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The effects of iCVD film thickness and conformality on the permeability and wetting of MD membranes

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Abstract
Membranes possessing high permeability to water vapor and high liquid entry pressure (LEP) are necessary for efficient membrane distillation (MD) desalination. A common technique to prepare specialized MD membranes consists of coating a hydrophilic or hydrophobic base membrane with a low surface-energy material. This increases its liquid entry pressure, making the membrane suitable for MD. However, in addition to increasing LEP, the surface-coating may also decrease permeability of the membrane by reducing its average pore size. In this study, we quantify the effects of initiated chemical vapor deposition (iCVD) polymer coatings on membrane permeability and LEP. We consider whether the iCVD films should have minimized thickness or maximized non-conformality, in order to maximize the permeability achieved for a given value of LEP. We determined theoretically that permeability of a single pore is maximized with a highly non-conformal iCVD coating. However, the overall permeability of a membrane consisting of many pores is maximized when iCVD film thickness is minimized. We applied the findings experimentally, preparing an iCVD-treated track-etched polycarbonate (PCTE) membrane and testing it in a permeate gap membrane distillation (PCMD) system. This study focuses on membranes with clearly defined, cylindrical pores. However, we believe that the principles we discuss will extend to membranes with more complex pore architectures. Overall, this work indicates that the focus of surface-coating development should be on minimizing film thickness, not on increasing their non-conformality.

Keywords: Membrane distillation (MD), Desalination, Track-etched polycarbonate (PCTE) membranes, Dusty gas model, Initiated chemical vapor deposition (iCVD).
### Variables

- \( a \): Ratio of uncoated/coated pore radii measured at top surface of membrane, \( a = \frac{r_o}{r_t} \)
- \( A_d \): Coefficient of molecular diffusion (kg/m\(^2\)-s-Pa)
- \( A_k \): Coefficient of Knudsen diffusion (kg/m\(^2\)-s-Pa)
- \( c \): Pore concentration on the membrane surface (pores/m\(^2\))
- \( c_{200} \): Pore concentration of Sterlitech’s 200 nm (radius) PCTE membrane
- \( d_e \): Collision diameter of water molecules (m)
- \( D \): Diffusion coefficient of water in air (m\(^2\)/s)
- \( K \): Permeability of membrane with pores of constant radius (kg/m\(^2\)-s-Pa)
- \( k_b \): Boltzmann constant (J/K)
- \( K_{iCVD} \): Permeability of membrane treated with an iCVD polymer coating (kg/m\(^2\)-s-Pa)
- \( K_{iCVD,\text{lin}} \): Permeability of membrane with iCVD coating approximated linearly (kg/m\(^2\)-s-Pa)
- \( K(x) \): Permeability of membrane at distance, \( x \), from its surface (kg/m\(^2\)-s-Pa)
- \( Kn \): Knudsen number ( )
- \( L \): Pore length = membrane thickness multiplied by tortuosity for straight pores (m)
- \( \Delta P \): Liquid entry pressure (Pa)
- \( P \): Total pressure within the pores during membrane distillation (Pa)
- \( p_a \): Partial pressure of air within the pores during membrane distillation (Pa)
- \( R \): Universal gas constant (J/K-mol)
- \( r \): Pore radius, constant value (m)
- \( r_t \): Pore radius at the membrane’s top surface (m)
- \( r_b \): Pore radius at the membrane’s bottom surface (m)
- \( r_o \): Pore radius prior to iCVD treatment (m)
1. Introduction

Membrane distillation (MD) is a thermal separation process used for desalination [1–5]. In direct contact and permeate gap membrane distillation (DCMD and PGMD), a hydrophobic membrane acts as a barrier separating the heated feed stream from the cooled distillate stream [6]. The temperature difference across the membrane creates a difference in the partial pressure between the water vapor on either side. This causes a net diffusion of water vapor through the membrane from the feed to the distillate. Salt and other contaminants in the feed stream are left behind.

The hydrophobic membrane in the MD system has two roles. It must be impermeable to liquid water, but permeable to water vapor. A high liquid entry pressure (LEP) ensures that liquid water does not enter the membrane. High permeability to water vapor is necessary to maintain efficient production of desalinated water [7–10]. Currently, MD systems primarily use hydrophobic membranes developed for micro- and ultra- filtration [5]. However, experimental, higher...
performance MD membranes are often prepared. Many of these membranes consist of a hydrophilic or hydrophobic base membrane coated with a low surface-energy chemistry to increase liquid entry pressure [11–16]. This versatile method increases the options for base membranes and surface chemistries, making it possible to produce higher performance membranes. However, while the hydrophobic surface treatment increases LEP, if it has thickness that is a significant fraction of pore radius, it will also change the membrane’s permeability to water vapor. The current study explores how the thickness and conformality of the hydrophobic coating affects the relationship between LEP and permeability. We also discuss how to maximize permeability for a given value of LEP.

2. Theoretical background

2.1. Models for LEP and permeability of an ideal membrane

MD membranes consist of a collection of pores. According to the Young-Laplace model [17], membranes consisting of cylindrical pores have LEP given by

\[ \Delta P = \frac{-2\gamma \cos(\theta)}{r_t} \quad \text{(Eq. 1)} \]

where \( \gamma \) is the liquid’s surface tension, \( \theta \) is the contact angle between the liquid and the membrane, and \( r_t \) is the pore radius at the surface of the membrane. For these ideal membranes, the only geometric quantity determining LEP is the pore radius at the membrane surface. Increasing this value decreases liquid entry pressure.

In contrast, permeability of a membrane to water vapor is affected by multiple aspects of the membrane architecture. For an ideal membrane consisting of straight, cylindrical pores, these factors include pore radius, pore concentration, and membrane thickness. MD membranes
typically have pore sizes ranging from 100 to 450 nm [5]. At this size range, the mean free path of water vapor, \( \lambda \), is comparable to the pore radius (Appendix A). This means that the Knudsen numbers, \( Kn = \lambda / 2r \), is within the transition regime (0.2 < \( Kn < 1.0 \)) in which both continuum and discrete effects are important. Although it has been met with some criticism [18], the permeability (often referred to as the membrane coefficient) for MD membranes is often described using the dusty gas model [19]. In the dusty gas model, the total resistance to diffusion is the sum of the resistances to molecular and Knudsen diffusion. This captures the effects of both the intramolecular and the wall collisions expected to occur at these \( Kn \) values.

The dusty gas model assumes that Knudsen and molecular diffusion are present in series within the pores [2]. The physical basis for the mechanisms being in series is still under debate [18]. A condensed version of the dusty gas model for a membrane consisting of cylindrical pores of radius, \( r \), length, \( L \) and concentration, \( c \) (pores/m\(^2\)) is given by

\[
K = \frac{A_d A_k}{A_d + A_k r} \frac{c r^3}{L} \tag{Eq. 2}
\]

where \( K \) is permeability and \( A_k \) is a constant of the system. \( A_k \) is defined as

\[
A_k = \frac{2 \pi M_w}{3} \frac{RT}{RT} (\frac{8RT}{\pi M_w})^{1/2} \tag{Eq. 3}
\]

where \( R \) is the universal gas constant (J/mol-K), \( T \) is temperature (K), and \( M_w \) is the molecular weight of water (g/mol). \( A_d \) is also a constant of the system. It is defined as

\[
A_d = \frac{\pi M_w P_D}{RT} \frac{P_D}{\rho_a} \tag{Eq. 4}
\]

where \( P \) is the total pressure inside the pores (Pa), \( D \) is the water diffusion coefficient with air (m\(^2\)/s) and \( \rho_a \) is the air pressure within the pores (Pa) [19]. According to Eq. (2), as \( r \) approaches zero (\( Kn >> 1 \)), \( K \) approaches pure Knudsen diffusion. As \( r \) becomes very large (\( Kn << 1 \)), \( K \)
approaches pure molecular diffusion. At intermediate values of $Kn$, both sources of resistance are significant, and permeability is lower than it would be for pure Knudsen or pure molecular diffusion. As seen in Eq. (2), permeability is highly sensitive to pore radius, increasing substantially with increased values of $r$.

As seen from Eq. (1) and Eq. (2), liquid entry pressure and permeability do not necessarily scale with each other. To produce more efficient MD membranes, it is desired to increase permeability without decreasing LEP beyond the limit needed to prevent liquid water entry. One way to do this is to modify the attributes of the membrane that affect permeability but do not affect LEP. These include membrane thickness, pore concentration and pore size below the surface of the membrane. In this study, we focus on pore size, determining how iCVD coatings affect the relationship between pore size at and below the surface of the membrane. We use knowledge of the pore profiles to predict how the iCVD coating will affect the relationship between permeability and LEP of the membrane.

2.2. Overview of iCVD film thickness and conformality

iCVD has been used previously to prepare hydrophobic membranes for MD and other applications [12, 16, 20–22]. A defining characteristic of iCVD coatings is the ability to make them ultra-thin (~10 nm) and the ability to tune their conformality. iCVD films are grown from vapor-phase monomer and initiating radicals. The monomer and initiating radicals enter the pores from the “top” surface of the membrane, polymerizing on the internal walls [23–25] (Fig. 1). Multiple factors influence the thickness of the iCVD film along the lengths of the pores. The
limit of uniform thickness in all locations is termed conformal coating. Reduction in film thickness with increased depth into the pore is termed non-conformal coating.

In an iCVD reactor, the membrane is placed on a stage and monomer and initiating radicals are introduced from one side (the "top" of the membrane). During the deposition, the diffusion rate of the monomer into the pores is fast with respect to the surface reaction rate (low Damköhler number). This is due to the relatively large pore size (~200 nm) and the slow deposition rate. Under this assumption, an equilibrium concentration of monomer is maintained on all surfaces of the membrane. However, unreacted initiating radicals in the gas phase are depleted with increasing depth into the pores. If the rate of polymerization is proportional to radical concentration, film-thickness decreases down the length of the pore, resulting in increased pore radius with increasing distance from the top surface.

![Diagram](image)

**Fig. 1.** Schematic drawing of a single pore during iCVD polymer deposition. $x$ indicates the distance from the top surface of the pore. $L$ is the length of the pore. $M$ is a monomer and $I$ is an initiating radical. The pore radius prior to iCVD coating is $r_o$. 

Assuming that the chemistry and surface energy of the iCVD coating are fixed, there are three main options for the iCVD coating profile (Fig. 2). These options have different implications for the permeability of the membrane.

**Fig. 2.** Schematic cross-sections four pore structure, with the base membrane is shaded dark grey and having a horizontal cylindrical pore of radius, \( r_o \). Structure (a) is an untreated membrane. The hydrophobic iCVD film is denoted in blue. For pores (b), (c) and (d), the thickness of the iCVD film varies down the length of the pores. However, the radius of the pore at the top surface, \( r_t \), is identical for all three coated pores. For (b) and (c), the iCVD thickness at the bottom of the pore is 90% that of the value at the top (\( S_L = 0.9 \) as defined in Eq. (5)). For (d) the variation in thickness is greater, with \( S_L = 0.1 \).

Fig. 2a shows a single uncoated cylindrical pore, with a small starting pore size. The radius of the pore at the top of the membrane, \( r_t \), equals the pore’s original, untreated radius, \( r_o \). Fig. 2b shows the membrane from Fig. 2a coated with an ultrathin, iCVD film. In this case, \( r_t \) is slightly less than \( r_o \) (\( r_o/r_t = 1.1 \)). In addition to being ultra-thin, the iCVD film in Fig. 2b has a high degree of conformally with a step coverage of \( S_L = 0.9 \). Step coverage is defined as the ratio of
coating thickness at the bottom and top of a pore. Smaller values of $S_L$ indicate coatings that are less conformal.

Fig. 2c shows a different way of achieving the same $r_t$ using iCVD. We hypothesize that having identical values of $r_t$ will result in identical values of LEP. In Fig. 2c, the starting pore radius, $r_o$, is larger and the iCVD coating is thicker than in Fig. 2b. The coated pore has $r_o/r_t = 4$. The step coverage is again highly conformal with $S_L = 0.9$. A third coating option expected to have the same LEP is illustrated in Fig. 2d. This pore has the same starting pore radius as Fig. 2c, and the same ratio of $r_o/r_t = 4$. However, the conformality of the film is significantly lower, with $S_L = 0.1$. While we anticipate the pores in Fig 2b – d will have the same LEP, differences in their permeability to water vapor are expected. In this study, we quantify how they differ.

2.3. Quantifying iCVD film thickness and conformality

In order to quantify the effects of non-conformality on the permeability of membranes, it is necessary to characterize the profile of the iCVD coating at all points within the membrane. This profile can be calculated based on the principles of the polymerization.

iCVD films are grown from vapor-phase monomer and initiating radicals that enter the pores from the “top” surface of the membrane (Fig. 1). As initiating radicals react with the monomer, they are depleted, reducing the rate of polymerization with increasing distance from the surface. The rate of depletion of initiated radicals with distance from the surface of the pore depends on a quantity called the sticking coefficient [24]. The sticking coefficient is controlled during iCVD deposition by the fractional saturation of the monomer in the deposition chamber. Low sticking
coefficients produce films that are nearly conformal (constant film thickness). Higher sticking coefficients cause steeper depletion and greater asymmetry of the film, producing pores increasingly similar to Fig. 2d.

The step coverage of iCVD polymer films has been studied previously [24]. Step coverage, $S_L$, can be written as

$$S_L = \frac{r_o - r_b}{r_o - r_t}$$ \hspace{1cm} (Eq. 5)

where $r_o$ is the unmodified pore radius. $r_t$ and $r_b$ are the top and bottom pore radii after iCVD treatment. Analytical modeling [24] has determined that

$$\ln (S_L) = -\frac{3\Gamma}{4} \left(\frac{L}{2r_o}\right)^2$$ \hspace{1cm} (Eq. 6)

where $\Gamma$ is the sticking coefficient of the initiator and $L$ is the length of the pore. This model assumes that the monomer and initiating radicals are in the Knudsen diffusion regime within the pore and so collide primarily with the pore walls. This is a reasonable assumption given the low pressure in the iCVD deposition chamber (< 1 Torr). Increasing the sticking coefficient or increasing the aspect ratio of the pores lowers the step coverage, producing less conformal coatings.

Eq. (5) can be generalized to describe the step coefficient at any distance $x$ from the top surface of the membrane. $S_L$ is replaced by $S(x)$ which is defined as

$$S(x) = \frac{r_o - r(x)}{r_o - r_t}$$ \hspace{1cm} (Eq. 7)

where $r(x)$ is the pore radius at distance $x$ from the top of the pore. Using the same analytical model as for Eq. (6), $S(x)$ is modeled as
\[
\ln(S(x)) = -\frac{3r}{4} \left(\frac{x}{2r_o}\right)^2 = \left(\frac{x}{L}\right)^2 \ln(S_L).
\]  
(Eq. 8)

As \(x\) approaches \(L\), \(S(x)\) approaches \(S_L\). Combining Eq. (7) and Eq. (8) and solving for \(r(x)\) produces an equation for \(r(x)\):

\[
r(x) = r_o - S_L \left(\frac{x}{L}\right)^2 (r_o - r_t).
\]  
(Eq. 9)

While the pore profile in Eq. (9) is implied in [24], this is the first time it has been calculated explicitly. Fig. 2d illustrates the predicted shape of a non-conformal iCVD coating profile. Knowledge of the pore profile makes it possible to calculate the effect of the iCVD film on permeability.

3. Materials and methods

3.1. Membrane preparation

In addition to building new theory, in this study we also prepared a membrane similar to the one in Fig. 2b, and tested it in a permeate gap membrane distillation (PGMD) system. We used polyvinylpyrrolidone (PVP) treated, hydrophilic, track-etched polycarbonate membranes (Sterlitech, PCT01214220) as the base membrane. We chose this membrane because its pore structure resembles an ideal membrane with straight cylindrical pores (Fig. 3). Pore size (diameter) was 400 nm. Total membrane thickness was 24 \(\mu\)m. Pore density was \(1.5 \times 10^{12}\) pores/m\(^2\).
Fig. 3. SEM images of the PCTE membrane (a) as-purchased (top view) (b) as-purchased (cross-section) and (c) after iCVD treatment (top view). The scale bars represent 5 µm. (d) A schematic of a pDVB (light grey)-pC6PFA (blue) bilayer iCVD coating on the PCTE membrane (dark gray). The iCVD film as shown is perfectly conformal.

We used initiated chemical vapor deposition (iCVD) [26] as a method to deposit a hydrophobic coating on the PCTE membranes. iCVD can deposit polymer films that range from ultra-thin to microns thick. The iCVD polymer used in this study was a bilayer of poly(divinyl benzene) (pDVB) and poly(1H, 1H, 2H, 2H-perfluorooctyl acrylate) (pC6PFA) (Fig. 3d). The cross-linking polymer, pDVB, forms a robust layer at the interface of the membrane. The pC6PFA forms an ultra-thin (<10 nm) layer on top of the pDVB to achieve a high contact angle with
water (110 - 135 °). Without the pDVB base layer, pC6PFA has significant side-chain rearrangement, reducing its contact angle hysteresis and making it less suitable use for MD [27, 28]. pDVB-pC6PFA bilayers have been studied as an environmentally friendly alternative to poly(1H, 1H, 2H, 2H-perfluorodecyl acrylate) (pPFDA). However, they have not been applied previously to MD membranes [27, 28].

Both iCVD layers were deposited in a custom-built reaction chamber. The chamber is cylindrical (height = 38 mm, diameter = 246 mm). It contains an array of 14 resistively heated parallel filaments (80% Ni, 20% Cr). Membranes were taped to a cooled stage (recirculating chiller/heater, NESLAB). The total pressure inside the chamber was maintained at a constant value using a mechanical pump (45 CFM pumping speed, Alcatel).

To produce the pDVB layer, tert-butyl peroxide (TBPO, Sigma-Aldrich, 97%) initiator and DVB (Sigma-Aldrich, 80%) monomer were introduced into the chamber. The TBPO was at room-temperature and was introduced at a rate of 1.0 sccm. The DVB was heated to 60 °C and introduced at a rate of 0.5 sccm. The stage was maintained at 30 °C, and the total pressure in the vacuum chamber was 800 mTorr. This resulted in a fractional saturation of the DVB monomer of 0.3. Deposition time of the pDVB layer was 189 minutes.

The pC6PFA layer was deposited directly on top of the pDVB film using the iCVD closed-batch configuration described previously [29]. The closed-batch configuration makes it easier to control film thickness for monomers that polymerize rapidly such as C6PFA. C6PFA monomer (Sigma-Aldrich, 97%), and TBPO (Sigma-Aldrich, 97%) were used. The chamber was initially
evacuated. The TBPO initiator was fed into the evacuated chamber at room temperature until the total pressure reached 110 mTorr. The C6PFA monomer was heated to 80 °C and fed into the chamber until the total pressure in the chamber was 190 mTorr. The stage was maintained at 25 °C. After filling the chamber with initiator and monomer, all valves were closed and the system was let rest for 2 minutes to allow mixing. The filament array was then turned on for 15 minutes, allowing the film to form. Next, the filaments were turned off and the chamber was evacuated. When the system had cooled, the chamber was refilled with initiator and monomer and the deposition process was repeated for a total of nine times. Depositing multiple rounds of C6PFA increased the pC6PFA layer thickness, reducing the possibility of defects due to thinness of the coating.

3.2. SEM imaging and pore size analysis

The pore radii at the top and bottom surfaces of the membrane was determined using image analysis of 445 µm², 5 nm/pixel resolution SEM images of the top and bottom surfaces of the membrane. This made it possible to characterize the step coverage of the pores in a way that bulk characterization would be unable to do. SEM images were collected using a JEOL 6010a SEM microscope with an acceleration voltage of 5 keV. All SEM samples were sputtered with gold to improve conductivity during imaging. The thickness of this gold layer was taken into account when calculating pore size. SEM images were read into MATLAB and converted to black and white using a threshold determined using Otsu’s method. Pores were identified and their areas were measured using MATLAB’s regionprops command. Pores with areas smaller than 500 pixels were discarded. The remaining pores were placed in a histogram with bin-size of 5 nm. The average (mode) pore size was determined by identifying the bin with the most pores and
calculating a radius assuming a circular pore-shape. Similar analysis using curve-fitting instead of mode value to determine average pore size, has been used by other researchers [30].

The pore size distribution of a representative membrane is shown in Fig. 4. The inset shows a section of the membrane with the centroids of the pores marked. Some overlapping pores can be seen which produce larger openings at the surface of the membrane. More work is needed to determine their exact effect on the LEP and permeability of the overall membrane.

Fig. 4. The pore size distribution of a 445 µm² section of an iCVD-treated membrane as determined using analysis of an SEM image. The inset is a small section of the processed image.

3.3. Angle resolved x-ray photo spectroscopy (ARXPS)

SEM imaging determined the total thickness of the iCVD coating. ARXPS was used to measure the thickness of just the pC6PFA layer on the treated membrane. ARXPS was conducted using a Surface Science Instruments SSX-100 with an operating pressure of ~2×10⁻⁹ Torr. A 4 keV Argon ion source was used with a beam current of 1 mA. We used angling of the beam to
measure the ratio of the F$_{S1}$ and C$_{S1}$ signals at a range of depths from the top and bottom surfaces of the membrane (where top is the direction from which the iCVD coating was deposited). Based on the inelastic mean free path of 2.4 nm, the depth of penetration of the x-ray beam was calculated to be 7.2, 6.2, 4.6 and 2.5 nm at incidence angles of 0, 30, 50 and 70 °, respectively. Measurements taken at each angle indicated the strength of the fluorine signal to each of these depths. F$_{S1}$/C$_{S1}$ for pure pC6PFA is 1.3 based on calculation from its chemical structure. Values below this indicate that the coating is incomplete when measured to that depth.

3.4. Contact angle, liquid entry pressure, and permeate gap membrane distillation (PGMD)

Advancing contact angles were measured using a goniometer equipped with an automatic dispenser (model 590, Ramé-Hart). DropImage software was used to acquire images for measurement. A 3 µL drop of room-temperature DI water was first placed onto the membrane surface. Water was then added to this drop in increments of 2 µL, and the angle between the advancing drop and the membrane surface was measured 100 ms after each addition.

Liquid entry pressure (LEP) was measured using a custom system similar to ones used previously [12, 16, 31, 32]. A pristine sample of the membrane was held in a 13 mm syringe membrane holder (GE healthcare biosciences). The membrane was exposed to the saline solution (35 g/L, NaCl) on one surface and deionized (DI) water on the other. A syringe pump (PHD 22/2000, Harvard apparatus) incrementally increased the pressure of the saline solution against the membrane. After each increase, the pressure was held constant for 12 seconds. A USB pressure transducer (PX409, Omega) monitored the pressure difference across the membrane. LEP is defined as the pressure at which liquid first passes through the membrane. The deionized
water reservoir was monitored using an electrical conductivity meter (Oakton Con6 Probe). LEP was detected by an increase in the electrical conductivity of the reservoir corresponding to a rate of 0.3 µL/s of saline entering the reservoir. This was the smallest rate that we could measure with our system. For all LEP testing, the active area of the membrane was 0.64 cm². Three samples from each membrane were tested for LEP.

Permeate gap membrane distillation (PGMD) was conducted using a custom-built lab-scale system. The active area of the membrane was rectangular with a surface area of 21 cm². The feed solution contained DI water and NaCl at a concentration of 35 g/L. Feed and distillate flowed past the membrane at a rate of 680 L/hr. Distillate temperature was maintained at 20 °C. Feed temperature was 40 – 60 °C. Experiment duration was 18 hours. When calculating the membrane distillation coefficient, temperature polarization was taken into account using previous simulations. This modelling included a simultaneous equation solver with discretized cells for heat and mass transfer balancing, solved with the finite difference method. It accounted for convection, conduction, evaporation, temperature polarization, etc [33]. Analysis was done and validated through comparisons to well-characterized membranes, with trials for numerous temperatures.

4. Results and discussion

4.1. Theoretical findings

4.1.1. Permeability of asymmetric membranes

The dusty gas model assumes pores that are cylindrical with unvarying pore radius within the membrane. In this study, we extend the dusty gas model to describe membranes with pores
whose radii vary lengthwise along the pore. This new model is described below with further
derivation in Appendix B.

Due to the iCVD coating, the membranes considered in this study have pores that are
asymmetric, with the pore radius varying with distance from the surface of the membrane. We
have not seen analysis of the permeability of such pores in the literature so we derive new
equations. If the pores have radii that vary with distance, \( x \), from the membrane surface, the
dusty gas permeability becomes

\[
K_{iCVD} = \frac{L}{\int_0^L \frac{1}{K(x)} \, dx}
\]  
(Eq. 10)

where \( K \) is a function of \( x \) and is defined in Eq. (2). This approach assumes that changes in \( r \) with
respect to \( x \) occur over length scales much larger than \( r \). It also assumes that the mean free path
of the gas is small compared to the rate of variation of \( r \) with respect to \( x \).

A closed-form solution for \( K_{iCVD} \) is not available when \( r(x) \) is defined by Eq. (9). However, a
closed-form solution would be useful to build intuition about the system. One such solution can
be obtained if we approximate \( r(x) \) as varying linearly in \( x \). In a linear approximation, \( r(x) \) is
described by

\[
r(x) = r_t + \frac{r_t(a-1)}{L} x
\]  
(Eq. 11)

where \( a \) is a measure of asymmetry defined as the ratio of the radius at the bottom of the pore
\((r_b)\) and the radius at the top of the pore \((r_t)\) so that \( a = r_b/r_t \). The pore radius is always larger at
the bottom of the pore so \( a \) is always greater than one. With this definition of \( r(x) \), the dusty gas
permeability of a membrane with asymmetric pores, \( K_{iCVD,lin} \), is given by
\[ K_{iCVD,lin} = \frac{2a^2A_dA_k}{A_d(a+1)+2A_kr_t} \frac{cr_t^3}{L}. \]  
(Eq. 12)

Eq. (12) can be rewritten as

\[ K_{iCVD,lin} = a \frac{A_dA_k}{A_d-\frac{(a+1)}{2a}A_kr_t} \frac{cr_t^3}{L}, \]  
(Eq. 13)

revealing that \( K_{iCVD,lin} \approx aK \).

4.1.2. Effect of iCVD films on membrane permeability

To theoretically compare the effects of different iCVD films on membrane permeability, we must compare membranes with the same value of \( r_t \) and LEP. We consider the ratio, \( R \), between the permeability of coated and uncoated pores with top pore radius, \( r_t \).

As was observed in Eq. (13), if both membranes have the same value of \( r_t \),

\[ R = \frac{K_{iCVD,lin}}{K} \approx a. \]  
(Eq. 14)

Since, unlike \( S_L \), \( a \) is not an experimentally controllable parameter, we use Eq. (5) to rewrite \( a \) in terms of \( S_L \):

\[ a = \frac{r_o}{r_t} - \left( \frac{r_o}{r_t} - 1 \right) S_L. \]  
(Eq. 15)

Eq. (14) thus becomes

\[ R \approx \frac{r_o}{r_t} - \left( \frac{r_o}{r_t} - 1 \right) S_L. \]  
(Eq. 16)

Eq. (16) shows that as \( S_L \) approaches zero, \( R \) approaches \( r_o/r_t \). As \( S_L \) approaches 1, \( R \) approaches 1. This implies that increasing \( r_o/r_t \) (i.e. increasing the iCVD film thickness) increases the permeability possible at a given value of \( r_t \) and LEP. This result is plotted in Fig. 5. The shaded area in Fig. 5 is the area between Eq. (16) evaluated for \( S_L = 0 \) and \( S_L = 1 \). The three additional curves show \( R \) evaluated using the exact equation for pore radius rather than the linear
approximation. These three curves, which are exact predictions of iCVD-treated membrane performance, lie within the envelope defined using the approximations.

![Graph showing the ratio of permeability of iCVD-coated and uncoated membranes](image)

**Fig. 5.** The ratio of the permeability of iCVD-coated and uncoated membranes, both with $r_t = 200$ nm. Pore concentration is constant across membranes. The insets illustrate the geometries of the pores on the lines that they overlap. Plotted on a log-log scale.

Fig. 5 suggests that permeability is maximized by maximizing thickness and non-conformality of the iCVD coatings. However, this is misleading. For real membranes, if the starting pore size, $r_o$, increases, the number of pores that can fit on the membrane decreases. If total porosity at the membrane surface is preserved precisely, pore density scales according to

$$c \sim \frac{1}{r_o^2}$$

(Eq. 17)

Taking this into account, $R$ is now multiplied by $\left(\frac{r_t}{r_o}\right)^2$. It now becomes

$$R \sim \left(\frac{r_o}{r_t} - \left(\frac{r_o}{r_t} - 1\right) S_L\right) \left(\frac{r_t}{r_o}\right)^2.$$

(Eq. 18)
According to Eq. (18), as $S_L$ approaches 1, $R$ approaches $\left(\frac{r_t}{r_o}\right)^2$. As $S_L$ approaches zero, $R$ approaches $\frac{r_t}{r_o}$. Since $r_t$ is always less than or equal to $r_o$, this indicates that increasing film thickness decreases permeability regardless of the level of asymmetry of the iCVD film. This result is shown in Fig. 6.

**Fig. 6.** The ratio of the permeability of iCVD-coated and uncoated membranes, both with $r_t = 200$ nm. Pore concentration scales according to Eq. (17). The insets illustrate the geometries of the pores on the lines that they overlap. Plotted on a log-log scale.

This analysis shows that if the base membrane is chosen to preserve porosity regardless of the uncoated membrane’s pore size, then increasing iCVD film thickness decreases permeability. This result is independent of whether the coating is conformal. This finding can be applied as follows. For example, Sterlitech sells many PCTE membranes, including ones with pore sizes (radius) of 200, 500, 1000 and 2500 nm (Table 1). These membranes have pore densities ranging
from $1.5 \times 10^{12}$ pores/m$^2$ for the 200 nm membrane, to $4 \times 10^9$ pores/m$^2$ for the 2500 nm membrane. If a value of $r_t = 200$ nm is needed to have adequate LEP for MD, we can compare the permeabilities of the three larger membranes after iCVD coating to $r_t = 200$ to the permeability of the 200 nm membrane without any coating. The results are shown in Table 1. What we find is that the 500, 1000 and 2500 nm membranes are predicted to have 33.25%, 6.65% and 3.375% the permeability of the uncoated 200 nm membrane after coating. This is assuming that limiting case of $S_L = 0$. This result illustrates that increasing the starting pore size and then narrowing the top of the pore using iCVD, ultimately causes a reduction in membrane permeability. In order to maximize permeability, a membrane with a pore size as close as possible to the desired value of $r_t$ should be chosen and the iCVD film thickness should be minimized.

Table 1. Predicted permeability of three membranes from the Sterlitech catalog after iCVD treatment. Permeability is expressed relative to the permeability of an uncoated membrane from the same catalog with $r_o = 200$ nm and pore concentration, $c_{200} = 1.5 \times 10^{12}$ pores/m$^2$. We assume the coated pore size at the surface of the membrane is $r_t = 200$ nm. The rightmost column is calculated by multiplying Eq. (16) by $c/c_{200}$ to account for differences in pore concentration between the different membranes. We assume that step coverage of the iCVD coating is $S_L = 0$. This is the limit of non-conformality.

| $r_o$ | $c$     | $r_o/r_t$ | $c/c_{200}$ | $R = K_{iCVD,lin}/K_{200}$ |
|------|---------|-----------|--------------|-----------------------------|
| 500  | $2 \times 10^{11}$ | 2.5       | 0.133        | 0.3325                      |
| 1000 | $2 \times 10^{10}$ | 5         | 0.0133       | 0.0665                      |
| 2500 | $4 \times 10^9$    | 12.5      | 0.0027       | 0.03375                     |
One exception to this finding is if a membrane can be produced that has large internal pore radii, where each large pore has many small openings at the membrane surface. This structure has the benefits of non-conformality/asymmetry without the accompanying reduction in pore density. Membranes such as this have been produced using phase inversion [13]. They could also potentially be prepared using free-standing, iCVD polymer films [34]. This type of membrane could have permeability that increases with $r_o/r_i$ according to Eq. (14). However, more work is needed to make this a viable option.

4.2. Experimental findings

4.2.1. Membrane characterization

With the insights about base membrane pore size and iCVD film thickness, we set out to prepare a membrane suitable for MD. For the base membrane, we chose a 200 nm radius PCTE membrane from Sterlitech. We deposited a pDVB-pC6PFA iCVD bilayer on the membrane, trying to minimize the thickness of the bilayer while maintaining the desired surface energy. Image analysis determined that the pDVB-pC6PFA bilayer was 20 nm thick at the top surface of the membrane and 5 nm thick at the bottom surface of the membrane (both measurements +/- 10 nm). This corresponds to step coverage, $S_L = 0.25$. Angle resolved XPS (ARXPS) was used to determine the contribution of the pC6PFA to the total bilayer thickness (Fig. 7). On the top surface, the pC6PFA layer on the top surface is at least 7.2 nm thick. On the bottom surface, the pC6PFA layer is slightly thinner than 2.5 nm. Both of these thicknesses are adequate to achieve the desired pC6PFA material properties.
Fig. 7. The ratio of the $F_{S1}$ and $C_{S1}$ ARXPS signals at four sampling depths from the top and bottom surfaces of the membrane. The inset shows a schematic of the area near the membrane’s top surface. The thickness of the pC6PFA film is indicated. The layer below the pC6PFA is the pDVB.

4.2.2. Membrane performance

We first verified that the pDVB-pC6PFA bilayer increased LEP enough to prevent wetting during MD testing. This was especially important because bilayer polymer films of this composition have never before been applied to MD membranes. We measured the apparent advancing contact angle (ACA) and LEP of a PCTE membrane as-purchased, after application of pDVB and after applications of the pDVB-pC6PFA bilayer (Table 2). Measurements showed that the bilayer-treated membrane has a water LEP of 276 kPa (LEP measurements were ± 21 kPa) This value is suitable for MD. The membrane treated with the pDVB layer only does not have an LEP high enough for successful MD performance. This indicates that the bilayer is necessary to prepare a membrane suitable for MD.
Table 2. Advancing contact angle (ACA) and liquid entry pressure (LEP) of PCTE membranes as-purchased, after application of pDVB and after application of the full pDVB-pC6PFA bilayer.

| Membrane                                      | $r_t$ (nm) | ACA (°) | LEP (kPa) (measured) | LEP (kPa) (Y-L) |
|-----------------------------------------------|------------|---------|----------------------|-----------------|
| As-purchased PCTE                            | 200        | 91      | 0                    | 13              |
| pDVB                                          | 193        | 103     | 53                   | 168             |
| pDVB-pC6PFA bilayer (Membrane M0)             | 180        | 124     | 276                  | 447             |

We compared the measured LEP values to the values calculated from the Young-Laplace model (Eq. (1)). We assumed surface tension, $\gamma = 0.072$ N/m. We found that for the three membranes in Table 2, the measured LEP value was less than the predicted value. This may be an effect of the “double-pores” at the surface seen in Fig. 3 and Fig. 4. Over-predicting LEP for PCTE membranes has been shown previously as well [35].

We tested the bilayer-treated membrane in a permeate gap membrane distillation (PGMD) system using NaCl solution at a concentration of 35 g/L. This test showed that the iCVD-treated PCTE membrane had 99.98% salt rejection. This indicates that the membrane did not wet in the MD system. This is the first demonstration of a pDVB-pC6PFA bilayer successfully being used to prepare a hydrophobic membrane with adequately high LEP for MD. The measured permeability (membrane distillation coefficient) of the membrane was $1.36 \times 10^{-6} \pm 3.4 \times 10^{-7}$ kg/m²-Pa-s (Fig. 8). This value is slightly lower than the values for other membranes currently
used for MD [5]. This is largely explained by the significantly lower porosity (~10% versus >70%) of the PCTE membranes compared to other MD membranes.

![Graph showing permeability vs pore radius](image)

**Fig. 8.** Permeability (membrane distillation coefficient) of the PCTE membrane treated with the iCVD pDVB-pC6FA bilayer. The membrane was tested in a PGMD system for 40 – 60 °C feed temperature and 20 °C distillate temperature. Feed was saline solution (35 g/L, NaCl). The dusty gas model for permeability ($K$) is shown as a dashed line. The dusty gas model for $S_L = 0.25$ ($K_{iCVD}$) is shown as a solid line.

In Fig. 8, the experimental membrane permeability is plotted along with the dusty gas model. The asymmetric dusty gas model (Eq. (10)) predicts higher permeability than the symmetric version (Eq. (2)) and decreases at a more constant rate with respect to pore radius. Interestingly, the membrane outperformed both forms of the dusty gas model. This may indicate that the dusty
gas model is not the correct model. However, it is also consistent with the lower than expected LEP, indicating that there may be unaccounted for factors that increase the effective pore size of the membrane such as “double-pores”. The parameter values used for these models are based on measurements of the system and can be found in Appendix C.

This experimental work shows that an iCVD coating can effectively raise the LEP of a PCTE membrane to a level where it can be used for MD. It also shows the limitations of trying to control and predict LEP and permeability of iCVD-coated PCTE membranes. Further experimental study could apply the pDVB-pC6PFA bilayer to membranes with more complex pore structures while still following the principle of minimizing film thickness according to the theoretical findings.

5. Conclusions

In this study, we analyzed the effects of iCVD surface-modification on the permeability and LEP of MD membranes. We developed new models for the iCVD coating profile and for the dusty gas permeability of asymmetric membranes. We found that non-conformality of the iCVD film cannot be used to improve membrane permeability at constant LEP and that the key to maximizing permeability is to choose a base membrane that allows iCVD film thickness to be minimized.

In addition to determining the theoretical effects of iCVD coatings on membrane performance, we also demonstrated how the theory relates to an experimental membrane. We prepared a track-etched polycarbonate (PCTE) membrane treated with an iCVD pDVB-pC6PFA bilayer.
We determined that the bilayer successfully increased the LEP of the membrane to a level adequate to distill water in a PGMD system. We sized the base membrane to minimize the iCVD film thickness in order to maximize permeability. However, we found that we were limited experimentally in how thin we could make the iCVD layer while maintaining the desired material properties. We also found that the membrane had lower LEP and higher permeability than we calculated. This may because overlapping pores increase the effective pore size of the membrane.

For future studies, we suggest the further exploration of free-standing iCVD films that may be used to produce membranes whose pores have multiple small openings. Further theoretical and experimental work is also needed to determine if these findings extend to membranes with more complex pore structures.

**Appendix A: Calculating Knudsen number**

The system parameters and Knudsen numbers of the experimental system are given in Table A1.

Mean free path is calculated according to $\lambda = \frac{k_B T}{\sqrt{2}\pi N_d d_e^2}$ and the Knudsen number is calculated according $Kn = \frac{\lambda}{2r}$.

| Variable                        | Value    |
|--------------------------------|----------|
| Boltzmann constant, $k_B$ (J/K) | $1.38 \times 10^{-23}$ |
| Average temperature, $T$ (K)   | 313      |
| Average pressure, \( P \) (kPa) | 101 |
| Collision diameter, \( d_e \) (m) | 2.64 \times 10^{-10} |
| Mean free path, \( \lambda \) (m) | 1.38 \times 10^{-7} |
| Pore radius, \( r \) (m) | 2.0 \times 10^{-7} |
| Knudsen number, \( Kn \) | 0.35 |

Appendix B: Derivations of asymmetric transport models

The process for deriving the asymmetric versions of the dusty gas model is as follows. To go from \( K \) (Eq. (2)) to \( K_{\text{CVD}} \) (Eq. (10)), we need to incorporate the effects of non-constant \( r(x) \) and non-constant \( dP/dx \). This results in the equation,

\[
K_{\text{CVD}} = K(x) \frac{L}{\Delta P} \left( -\frac{dP}{dx} \right). \tag{Eq. B1}
\]

Rearranging and taking the integral with respect to \( x \) on both sides, this becomes

\[
\int_0^L K_{\text{CVD}} \, dx = \int_0^L \frac{L}{\Delta P} \left( -\frac{dP}{dx} \right) \, dx. \tag{Eq. B2}
\]

Simplify Eq. (B2), results in

\[
K_{\text{CVD}} \int_0^L \frac{1}{K(x)} \, dx = L. \tag{Eq. B3}
\]

Eq. (B3) rearranges to Eq. (10).

To go from Eq. (10) to Eq. (12), we use a change of variables from \( x \) to \( r \) so that Eq. (10) becomes

\[
K_{\text{CVD}, \text{lin}} = \frac{L}{\int_{r_t}^{r_u} \frac{1}{K(r)} \frac{dr}{dx}}. \tag{Eq. B4}
\]
Using the linear approximation for \( r(x) \) in Eq. (11), Eq. (B4) can be solved to produce Eq. (12). When evaluating \( K_{CVD} \) (Eq. (10)) numerically in MATLAB, rectangular numerical integration with a step-size of 0.1 nm was used.

**Appendix C: Parameter values for permeability models**

**Table C1.** Parameter values for the permeability models in Fig. 8.

| Parameter                                                                 | Value     |
|---------------------------------------------------------------------------|-----------|
| Diffusion coefficient of water in air multiplied by total pressure, \( PD \) (Pam\(^2\)/s). \( PD = 1.895(T^{2.072})10^{-5} \) \[19\] | 2.70      |
| Total average pressure, \( P \) (kPa)                                    | 101       |
| Molecular weight of water, \( M_w \) (g/mol)                             | 18        |
| Universal gas constant, \( R \) (J/K-mol)                                | 8.314     |
| Average temperature, \( T \) (K)                                        | 313       |
| Partial pressure of air, \( p_a \) (kPa)                                | 101       |

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