Value of fusion of PET and MRI in the detection of intra-pelvic recurrence of gynecological tumor: comparison with 18F-FDG contrast-enhanced PET/CT and pelvic MRI

Kazuhiro Kitajima · Yuko Suenaga · Yoshiko Ueno · Tomonori Kanda · Tetsuo Maeda · Natsuko Makihara · Yasuhiro Ebina · Hideto Yamada · Satoru Takahashi · Kazuro Sugimura

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Abstract

Background  To evaluate the diagnostic value of retrospective image fusion from pelvic magnetic resonance imaging (MRI) and 18F-fluorodeoxyglucose positron emission tomography (PET) in detecting intra-pelvic recurrence of gynecological tumor.

Methods  Thirty patients with a suspicion of recurrence of gynecological malignancy underwent inline contrast-enhanced PET/computed tomography (CT) and pelvic contrast-enhanced MRI for restaging. Diagnostic performance about the local recurrence, pelvic lymph node and bone metastasis and peritoneal lesion of PET/low-dose non-enhanced CT (PET/ldCT), PET/full-dose contrast-enhanced CT (PET/ceCT), contrast-enhanced MRI, and retrospective image fusion from PET and MRI (fused PET/MRI) were evaluated by two experienced readers. Final diagnoses were obtained by histopathological examinations, radiological imaging and clinical follow-up for at least 6 months. McNemar test was employed for statistical analysis.

Results  Documented positive locally recurrent disease, pelvic lymph node and bone metastases, and peritoneal dissemination were present in 53.3, 26.7, 10.0, and 16.7 %, respectively. Patient-based sensitivity for detecting local recurrence, pelvic lymph node and bone metastasis and peritoneal lesion were 87.5, 87.5, 100 and 80.0 %, respectively, for fused PET/MRI, 87.5, 62.5, 66.7 and 60.0 %, respectively, for contrast-enhanced MRI, 62.5, 87.5, 66.7 and 80.0 %, respectively, for PET/ceCT, and 50.0, 87.5, 66.7 and 60.0 %, respectively, for PET/ldCT. The sensitivity of diagnosing local recurrence by fused PET/MRI was significantly better than that of PET/ldCT (p = 0.041). The patient-based sensitivity, specificity and accuracy for the detection of intra-pelvic recurrence/metastasis were 91.3, 100 and 93.3 % for fused PET/MRI, 82.6, 100 and 86.7 % for contrast-enhanced MRI, 82.6, 100 and 86.7 % for PET/ceCT, and 71.4, 100 and 83.7 % for PET/ldCT.

K. K. Kitajima (✉) · Y. Suenaga · Y. Ueno · T. Kanda · T. Maeda · S. Takahashi · K. Sugimura
Department of Radiology, Kobe University Graduate School of Medicine, 7-5-2 Kusunoki-cho, Chuo-ku, Kobe 650-0017, Japan
e-mail: kitajima@med.kobe-u.ac.jp; kazu10041976@yahoo.co.jp
Y. Suenaga
e-mail: suenaga@med.kobe-u.ac.jp
Y. Ueno
e-mail: yono121@med.kobe-u.ac.jp
T. Kanda
e-mail: kanada@med.kobe-u.ac.jp
T. Maeda
e-mail: maeda@med.kobe-u.ac.jp
S. Takahashi
e-mail: takahashisato@med.kobe-u.ac.jp
K. Sugimura
e-mail: sugimura@med.kobe-u.ac.jp

K. K. Kitajima · Y. Suenaga · Y. Ueno · T. Kanda · T. Maeda · N. Makihara · Y. Ebina · H. Yamada · S. Takahashi · K. Sugimura
Department of Radiology, Hyogo Cancer Center, Hyogo, Japan
e-mail: makiharana@med.kobe-u.ac.jp
Y. Ebina
e-mail: ebinaa@med.kobe-u.ac.jp
H. Yamada
e-mail: yamada-hide@med.kobe-u.ac.jp
N. Makihara · Y. Ebina · H. Yamada
Department of Obstetrics and Gynecology, Kobe University Graduate School of Medicine, 7-5-2 Kusunoki-cho, Chuo-ku, Kobe 650-0017, Japan
and 86.7 % for PET/ceCT and 78.3, 85.7 and 80.0 % for PET/ldCT.

Conclusion Fused PET/MRI combines the individual advantages of MRI and PET, and is a valuable technique for assessment of intra-pelvic recurrence of gynecological cancers.

Keywords Fused PET/MRI · PET/CT · MRI · Restaging · Gynecological tumor

Introduction

Inline positron emission tomography/computed tomography (PET/CT), a combination of PET and CT with 18F-fluorodeoxyglucose (18F-FDG), is now accepted as a powerful imaging modality in evaluating various kinds of malignancies including gynecological cancers [1, 2]. PET/CT has been reported to be more useful than PET alone, with helpful anatomical and morphological information from its CT portion.

However, contrast resolution of CT for different tissues is limited especially in the pelvis and head and neck even when full-dose exposure and contrast medium are employed. In contrast, magnetic resonance imaging (MRI) has several advantages over CT, such as high tissue contrast and no radiation exposure. Because of the higher tissue contrast by MRI in gynecological cancers than with CT, fusion of MR and PET images (fused PET/MRI) may result in some clinical advantages for gynecological cancers over PET/CT. However, the clinical application of fused PET/MRI of the pelvis in gynecological cancer patients is still limited [3–5].

Moreover, although inline whole-body PET/MRI has been developed recently, it remains unknown whether the device is clinically applicable. To begin with, the clinical value of image fusion from MRI and PET in the gynecological disease needs to be clarified. The purpose of this study was to evaluate the validity of retrospectively fused PET/MRI obtained from different scanners for assessing intra-pelvic recurrence of gynecological cancers and to compare the diagnostic accuracy of fused PET/MRI with that of inline PET/full-dose contrast-enhanced CT (PET/ceCT) and PET/low-dose non-enhanced CT (PET/ldCT) with 18F-FDG, and contrast-enhanced MRI.

Materials and methods

Patients

This retrospective study was approved by the institutional review board in our institute, and the need for patient informed consent was waived. From December 2011 to January 2013, thirty patients (mean age 61.3 years; age range 38–83 years) previously treated for uterine cervical cancer (n = 15), ovarian cancer (n = 9) and endometrial cancer (n = 6) underwent conventional 18F-FDG PET/CT scan with low-dose CT (ldCT) followed by full-dose with IV contrast (ceCT) and pelvic contrast-enhanced MRI with a suspicion of recurrence including elevated tumor marker levels, abnormal CT or MRI findings, or an abnormal Papanicolaou smear. All patients received the histopathological result by biopsy or surgery, or clinical follow-up including PET/CT, CT, and MRI examinations for longer than 6 months. The maximum interval between MRI and PET/CT acquisition was 21 days (mean 7.7 days; range 0–21 days).

Pelvic MRI

All subjects were examined using a 1.5 T MR scanner (Achieva 1.5 T, Philips Medical Systems, Best, The Netherlands) with a pelvic phased-array coil. No intramuscular injection of butyl scopolamine or glucagon was used. Unenhanced T1-weighted images (T1WIs) were acquired in the axial and sagittal planes with a spin-echo repetition time (TR)/echo time (TE) = 525–702/5.5–9.8 ms sequence, 4–5 mm slice thickness/1 mm gap, a 20–24 cm field of view, and a 192 × 256 matrix. Axial, sagittal and coronal T2-weighted fast-spin-echo images (T2WIs); 3,500–4,600/90 ms, 4–5 mm slice thickness/1 mm gap, a 20–24 cm field of view, and a 192 × 256 matrix) were obtained. Axial diffusion weighted imaging (DWI) with b value of 0 and 1,000 ms were also obtained. After administration of 0.08–0.1 mmol/kg of gadolinium diethylenetriaminepentaacetic acid (DTPA) (Magnevist: Bayer Schering Pharma, Osaka, Japan), we obtained T1-weighted fat-suppressed axial, sagittal, and coronal sequences sequentially, with parameters similar to those used before the gadolinium DTPA injection.

18F-FDG contrast-enhanced PET/CT (PET/ceCT)

Whole-body imaging was performed using a combined PET/CT scanner (Discovery PET/CT 690, GE Healthcare, Waukesha, WI, USA). CT covered a region ranging from the meatus of the ear to the midthigh. The technical parameters of the 16-detector row helical CT scanner were a helical pitch of 28 or a beam pitch of 1.75, a gantry rotation speed of 0.6 s, and a slice thickness of 3.27 mm. The PET component of the combined imaging system allows simultaneous acquisition of 47 transaxial PET images with an interslice spacing of 3.27 mm in one bed position and provided an image from the meatus of the ear to the midthigh with 7–8 bed positions. The transaxial field of view and axial field of view of the PET images
reconstructed for fusion were 60 and 15.0 cm, respectively, with a matrix size of 192 × 192. To avoid artifacts caused by the urinary tract, patients were asked to drink 500 ml of water 1–2 h prior to image acquisition, and to void just before the start of acquisition. No urinary bladder catheterization was used. After at least 4 h of fasting, patients received an intravenous injection of 222–333 MBq (6–9 mCi) of $^{18}$F-FDG. The blood glucose levels were checked in all patients before FDG injection and no patients showed a blood glucose level of more than 160 mg/dL.

About 50 min later, initially ldCT was performed at 120 kV and Smart mA (20–120 mA, Noise Index 30) with the normal expiration position for attenuation correction of PET image. A whole-body emission PET scan was performed immediately after the ldCT, with a 2-min acquisition per bed position using a three-dimensional acquisition mode. Attenuation-corrected PET images were reconstructed with an ordered-subset expectation maximization iterative reconstruction algorithm called VUE Point FX-S with TOF and sharp IR (18 subsets, 2 iterations).

Finally, diagnostic ceCT was performed for the same axial coverage at 140 kV and Auto mA (20–300 mA, Noise Index 10) and 35.0 mm/rotation speed, during breath hold with the normal expiration positions, similar to ldCT scanning. Iodinated contrast material (Iopamiron Inj, Syringe, Bayer Schering Pharma, Berlin, Germany) containing 300 or 370 mg of iodine per milliliter at a dose of 450 mg of iodine per kilogram of body weight was intravenously administered by using a power injector with a fixed injection duration of 50 s. The scan of neck–thorax and abdomen–pelvis was started at 50 and 100 s, respectively, after injection. No oral contrast agent was administered. For image fusion, 3.27 mm slice was reconstructed. The ldCT, ceCT, and PET images were transferred to a commercially available workstation (Advantage Windows Workstation, version 4.5; GE Healthcare Europe) to access all data (Fig. 1).

Fused PET/MRI

PET and all MRI series (T1WI, T2WI and contrast-enhanced imaging) were retrospectively and manually fused using a dedicated, commercially available software (Advantage Windows Workstation, version 4.5, GE Healthcare Technology). This automatic rigid fusion software has already been used in other studies for image fusion of PET and MRI [3, 5, 6]. MR and PET/CT images were stored in a common database and the MR images were registered to CT images of PET/CT using a semi-automatic voxel-based algorithm. After registration, the coregistered images were reconstructed and visualized in the axial planes. Alignment in all three planes (axial, coronal, and sagittal) was assessed by checking the body outline and the position of metabolically active motionless organs (bone and spine). When the accurate image fusion was not feasible, PET–MRI fusion was evaluated by assessing PET/MRI-fused images side by side with PET and MRI images.

Image analysis

Images were analyzed on a dedicated workstation (Advantage Windows, version 4.5; GE Healthcare Europe). Two board-certificated radiologists/nuclear medicine physicians (both having double board-certifications) who are especially experienced in gynecology imaging, consensually and retrospectively evaluated MRI, PET/ceCT, PET/ldCT, and fused PET/MRI for the following findings: (a) local pelvic recurrence, (b) pelvic lymph node metastasis, (c) pelvic bone metastasis, and (d) peritoneal dissemination in consensus. Neither reader was aware of the results of other imaging studies, histopathologic findings or the clinical data. Each dataset was reviewed with the consensus of the two readers after a minimum interval of 3 weeks to avoid any decision threshold bias due to reading-order effects.

We referred several previous standard criteria about restaging gynecological cancer on MRI [7–9] and PET/CT interpretation [10, 11]. On MRI interpretation, lymph node swelling larger than 1 cm in short-axis diameter was graded as metastasis. On PET/CT and fused PET/MR interpretations, the classification of LNs as cancer positive was based on the presence of focally appreciable metabolic activity above that of comparable normal structures or surrounding tissue, with the exclusion of physiological bowel, vessel, and urinary activity [12]. Furthermore, the presence of a central unenhancing area suggesting central necrosis and the presence of peripheral low attenuation suggesting a fatty hilum within an LN was considered a benign sign.

Standard of reference

Histopathological correlation was available in 16 patients and was used as the standard of reference. In the remaining 14 patients, the results of treatment change and clinical follow-up of at least 6 months including PET/CT, CT and MRI examinations served as reference. We classified as recurrence and/or metastasis the cases if, for example, (1) the present study revealed highly suspected recurrence without pathological evidence and the patient underwent chemotherapy resulting in a decrease or disappearance in size and/or FDG uptake in the follow-up study and (2) the follow-up study revealed tumor recurrence with CT and/or PET/CT in a place where a tiny lesion without FDG uptake was imaged at the time of the initial (present) study (Fig. 2).
Statistical analysis

The McNemar test was used to determine the statistical significance of differences in the sensitivity, specificity and accuracy as determined by PET/ceCT, PET/ldCT, MRI, and fused PET/MRI. Statistical analysis was performed with SAS software version 9.3 (SAS Institute, Cary, NC). A p value less than 0.05 was considered to indicate a statistically significant difference.

Result

Documented positive locally recurrent disease, pelvic lymph node and bone metastases, and peritoneal dissemination were present in 16 of 30 patients (53.3 %), 8 of 30 (26.7 %), 3 of 30 (10.0 %), and 5 of 30 (16.7 %), respectively. 16 patients had recurrence in only one of the four sites, five had recurrence in two sites, and two had recurrence in three sites. Seven patients proved to have no intra-pelvic recurrent or metastatic lesions.

On per patient basis, the sensitivity, specificity and accuracy for the detection of intra-pelvic local recurrence were 87.5 % (14/16), 100 % (14/14) and 93.3 % (28/30) for fused PET/MRI protocol, 87.5 % (14/16), 100 % (14/14) and 93.3 % (28/30) for contrast-enhanced MRI protocol, 62.5 % (10/16), 100 % (14/14) and 80.0 % (24/30) for PET/ceCT protocol, and 50.0 % (8/16), 100 % (14/14) and 73.3 % (22/30) PET/ldCT protocol (Table 1). The sensitivity and accuracy of diagnosing local recurrence by fused PET/MRI were both significantly better than that of PET/ldCT (p = 0.041). There were no significant differences of
sensitivity ($p = 0.14$) and accuracy ($p = 0.14$) between fused PET/MRI and PET/ceCT protocols. The patient-based sensitivity, specificity and accuracy for the detection of pelvic lymph node metastasis were 87.5% (7/8), 100% (22/22) and 96.7% (29/30) for fused PET/MRI protocol, 62.5% (5/8), 100% (22/22) and 90.0% (27/30) for contrast-enhanced MRI protocol, 87.5% (7/8), 100% (22/22) and 96.7% (29/30) for PET/ceCT protocol and 87.5% (7/8), 95.5% (21/22) and 93.3% (28/30) for PET/ldCT protocol (Table 1). There were no significant differences of between fused PET/MRI and other protocols. The patient-based sensitivity, specificity and accuracy for the detection of peritoneal dissemination were 80.0% (4/5), 100% (25/25) and 96.7% (29/30) for fused PET/MRI protocol, 60.0% (3/5), 100% (25/25) and 93.3% (28/30) for contrast-enhanced MRI protocol, 80.0% (4/5), 100% (25/25) and 96.7% (29/30) for PET/ceCT protocol and 60.0% (3/5), 96.0% (24/25) and 90.0% (27/30) for PET/ldCT protocol (Table 1). There were no significant differences of between fused PET/MRI and other protocols.

The patient-based sensitivity, specificity and accuracy for the detection of intra-pelvic recurrence/metastasis were 91.3% (21/23), 100% (7/7) and 93.3% (28/30) for fused PET/MRI protocol, 82.6% (19/23), 100% (7/7) and 86.7% (26/30) for contrast-enhanced MRI protocol, 82.6% (19/23), 100% (7/7) and 86.7% (26/30) for PET/ceCT protocol and 78.3% (18/23), 85.7% (6/7) and
To our knowledge, this is the first reported study to have investigated the validity of retrospectively fused PET/MRI obtained from different scanners for assessing intra-pelvic recurrence of gynecological cancers and to compare the diagnostic accuracy of fused PET/MRI with that of contrast-enhanced PET/CT using $^{18}$F-FDG and pelvic contrast-enhanced MRI. Among three modalities, fused PET/MRI showed the highest sensitivity and accuracy. This result may be because of excellent spatial resolution and soft-tissue contrast of MRI and functional method based on the increased glucose metabolism of cancer cells, regardless of node size of $^{18}$F-FDG PET/CT [10].

There has been only one study to evaluate the additional diagnostic value of fused PET/MRI in the detection of pelvic and para-aortic metastatic lymph nodes in uterine cervical cancer patients. Kim et al. [3] demonstrated that in a study of seventy-nine patients with FIGO stage IB–IVA cervical cancer, region-based sensitivity, specificity and area under the receiver operating characteristic (ROC) of detecting pelvic and para-aortic lymph node metastases were 54.2 %, 92.7 % and 0.735 for fused PET/MRI, and those figures were 44.1 %, 93.9 % and 0.690 for PET/CT. They also reported a significant difference of ROC analysis ($p = 0.045$); however, we suppose the inferiority of PET/CT result may arise because contrast-enhanced medium was not used in CT scan of PET/CT study. In our series of PET/CT with contrast-enhanced medium, the difference was not observed between fused PET/MRI and PET/ceCT. $^{18}$F-FDG PET is a functional method based on the increased glucose metabolism of cancer cells, regardless of node size and PET/CT can often detect tiny metastatic LN from 5 to 9 mm in size which could not be diagnosed by CT or MRI [12]. In general, the sensitivity of diagnosing lymph node metastases by PET/CT is higher than that of CT or MRI.

Antonsen et al. [13] compared the primary tumor and nodal staging of endometrial cancer between preoperative contrast-enhanced PET/CT using $^{18}$F-FDG and contrast-enhanced MRI. They demonstrated that in a study of 318 patients with FIGO stage IA–IVB endometrial cancer, PET/ceCT and contrast-enhanced MRI were equal in predicting ≥50 % myometrial invasion, uterine serosa, cervical involvement and lymph node metastases. The sensitivity and specificity of detecting ≥50 % myometrial invasion were 93 and 49 % for PET/CT and 87 and 57 % for MRI. The sensitivity and specificity of detecting uterine serosa invasion were 75 and 99 % for PET/CT and 67 and 96 % for MRI. The sensitivity and specificity of cervical

### Table 1 Comparison of fused PET/MR, PET/CT and MRI for diagnosing intra-pelvic recurrence on a per patient basis

|                      | Fused PET/ MR (%) | MRI (%) | PET/ceCT (%) | PET/ldCT (%) |
|----------------------|-------------------|---------|--------------|--------------|
| **Local recurrence** |                   |         |              |              |
| Sensitivity          | 87.5 (14/16)      | 87.5 (14/16) | 62.5 (10/16) | 50.0 (8/16)  |
| Specificity          | 100 (14/14)       | 100 (14/14) | 100 (14/14)  | 100 (14/14)  |
| Accuracy             | 93.3 (28/30)*     | 93.3 (28/30) | 80.0 (24/30) | 73.3 (22/30)* |
| **Pelvic lymph node metastasis** |       |         |              |              |
| Sensitivity          | 87.5 (7/8)        | 62.5 (5/8) | 87.5 (7/8)   | 87.5 (7/8)   |
| Specificity          | 100 (22/22)       | 100 (22/22) | 100 (22/22)  | 95.5 (21/22) |
| Accuracy             | 96.7 (29/30)      | 90.0 (27/30) | 96.7 (29/30) | 93.3 (28/30) |
| **Bone metastasis**  |                   |         |              |              |
| Sensitivity          | 100 (3/3)         | 66.7 (2/3) | 66.7 (2/3)   | 66.7 (2/3)   |
| Specificity          | 100 (27/27)       | 100 (27/27) | 100 (27/27)  | 100 (27/27)  |
| Accuracy             | 100 (30/30)       | 96.7 (29/30) | 96.7 (29/30) | 96.7 (29/30) |
| **Peritoneal dissemination** |         |         |              |              |
| Sensitivity          | 80.0 (4/5)        | 60.0 (3/5) | 80.0 (4/5)   | 60.0 (3/5)   |
| Specificity          | 100 (25/25)       | 100 (25/25) | 100 (25/25)  | 96.0 (24/25) |
| Accuracy             | 96.7 (29/30)      | 93.3 (28/30) | 96.7 (29/30) | 90.0 (27/30) |

* PET/ceCT PET/full-dose contrast-enhanced CT, PET/ldCT PET/low-dose non-enhanced CT

|                      | PET/ceCT (%) | PET/ldCT (%) |
|----------------------|--------------|--------------|
| **Regional staging** |              |              |
| Sensitivity          | 87.5 (14/16) | 87.5 (14/16) |
| Specificity          | 100 (14/14)  | 100 (14/14)  |
| Accuracy             | 93.3 (28/30) | 93.3 (28/30) |

80.0 % (24/30) for PET/ldCT protocol. Among four modalities, fused PET/MRI showed the highest sensitivity and accuracy. However, the difference did not reach significant difference about the sensitivity ($p = 0.48$), specificity ($p = 1$), and accuracy ($p = 0.48$).
involvement were 43 and 94 % for PET/CT and 33 and 95 % for MRI. The sensitivity and specificity of detecting para-aortic and pelvic lymph node metastases were 74 and 93 % for PET/CT and 59 and 93 % for MRI.

In this study, PET/MR images were generated from PET and MR images obtained from different scanners and PET and MR images were merged and registered manually on a workstation. A drawback of the PET/MRI fusion images is misregistration due to the movement of organs between the PET and MRI studies. Pelvic organs may show little respiratory movement, but urinary volume and location of gas in the intestine, colon, and rectum may affect the location of surrounding organs. Inline PET/MRI technology may be expected to minimize these drawbacks of the PET/MRI fusion strategy and generate better image quality for fusion images (Fig. 3).

This study has several limitations. First, this was a retrospective study. PET/CT was not performed in every case of restaging gynecological cancer during the study period. The application of PET/CT to only selected cases might cause bias and influence the study results. The size of patient sample was relatively small. Further prospective and larger studies are needed. Second, the ideal gold standard for any analysis would be histological confirmation of the findings. However, clinical follow-up is a valid way to evaluate diagnostic accuracy and response to therapy, and it would have been unethical to investigate all imaging-detected lesions using invasive procedures. Positive findings are easy to confirm, but negative findings only mean that it is not possible to acquire positive findings during the follow-up period, making it uncertain whether the findings are truly negative. Therefore, sensitivity in this series may have been overestimated. Third, pelvic MR images but not whole-body MR images were used for PET/MRI fusion images. Therefore, intra-pelvic status was evaluated in our series. For a comparative study of diagnostic ability for distant metastasis, whole-body MRI is needed for the fusion images.

Conclusion

Fused PET/MRI, combining the individual advantages of MRI and PET, is a very useful modality for assessing intra-pelvic recurrence of gynecological cancers. The combination of whole-body PET and MRI into single scanner is a very promising diagnostic modality for oncological imaging due to the missing radiation exposure and the high soft tissue resolution of MRI in contrast to CT.

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Conflict of interest We declare no financial support or relationship that may pose conflict of interest.

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