Actin kinetics shapes cortical network structure and mechanics

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The actin cortex of animal cells is the main determinant of cellular mechanics. The continuous turnover of cortical actin filaments enables cells to quickly respond to stimuli. Recent work has shown that most of the cortical actin is generated by only two actin nucleators, the Arp2/3 complex and the formin Diaph1. However, our understanding of their interplay, their kinetics, and the length distribution of the filaments that they nucleate within living cells is poor. Such knowledge is necessary for a thorough comprehension of cellular processes and cell mechanics from basic polymer physics principles. We determined cortical assembly rates in living cells by using single-molecule imaging in combination with stochastic simulations. We find that formin-nucleated filaments are, on average, 10 times longer than Arp2/3-nucleated filaments. Although formin-generated filaments represent less than 10% of all actin filaments, mechanical measurements indicate that they are important determinants of cortical elasticity. Tuning the activity of actin nucleators to alter filament length distribution may thus be a mechanism allowing cells to adjust their macroscopic mechanical properties to their physiological needs.

INTRODUCTION

The skeleton of animal cells is composed of polymers that continuously undergo turnover of their proteic components (1–4). This holds notably for actin-based structures such as the cortex of animal cells, a submembranous shell that is the main determinant of cell shape and endows cells with their mechanical properties (5, 6). The cortex is a roughly isotropic polymeric network of semiflexible actin filaments [filamentous actin (F-actin)] cross-linked by specialized actin-binding proteins and containing motor proteins that generate stress within the network. The continuous turnover of cortical actin filaments enables animal cells to quickly respond to external stimuli and readily adapt to mechanical cues or biochemical signaling. In consequence, the cortex plays a central role in many biological processes such as cell division (7–9), motility (1, 3, 4), and tissue morphogenesis (5).

Despite its importance, our understanding of cortical organization and mechanical properties from the bottom-up is poor. In particular, the role of actin turnover kinetics for determining cortical network characteristics remains unclear. This is in part due to difficulties in deriving reaction constants for the turnover of individual actin filaments from fluorescence measurements on filament populations in living cells. Consequently, the relationship between actin turnover and cortex mechanics is largely unclear.

The major determinants of cortical mechanics are the density and lengths of the actin filaments, as well as the nature and density of the proteins cross-linking them (1–6, 8, 10–14). Direct measurement of the filament length distribution by fluorescence or electron tomography is currently impossible due to limited resolution and artifacts introduced by sample preparation, respectively. An alternative approach is to measure the kinetics of the biochemical turnover processes that control cortical actin filament density and length. However, whereas a large body of work on actin turnover exists in vitro (15–17), little is currently known about F-actin turnover kinetics in living cells. To add further complication, two filament subpopulations with effective turnover rates differing by a factor of ~20 have been shown to constitute the cortex (1, 3, 4, 18). These subpopulations are generated by distinct nucleation pathways, necessitating either formins or the Arp2/3 complex. Recent work has confirmed that these nucleators alone generate most of the cortical actin (19). Although in vitro experiments indicate that these two nucleator types have very different kinetics of polymer elongation (15, 17), our understanding of how these kinetics lead to distinct filament turnover times in vivo remains rudimentary. Consequently, the derivation of cortical mechanical properties, cortex thickness, and cortical actin filament length distribution from polymer physics theories is currently not possible (20–22).

One common method for quantifying actin turnover kinetics in living cells is the use of fluorescence recovery after photobleaching (FRAP) experiments (23), in which a micrometer-sized region is exposed to high laser power and the recovery of fluorescence intensity is monitored over time (24, 25). Actin filaments can only gain and lose monomers from their two extremities, respectively referred to as the barbed and pointed ends. The exchange of individual monomers in the cortex thus depends on a monomer’s position in a filament, and the interpretation of coarse-grained measurements in terms of molecular reaction rate constants is challenging. Moreover, filaments can be severed, which does not lead to changes in the fluorescence, but increases the difficulty of interpreting the fluorescence data even further.

Here, we used single-molecule fluorescence imaging and stochastic simulations to quantitatively characterize the molecular processes underlying cortical actin filament network assembly in vivo. From these data, we derived the average lengths of formin- and Arp2/3-nucleated cortical filaments. We found that less than 10% of the filaments, containing 20 to 25% of actin protomers incorporated in filaments, were nucleated by formins. Surprisingly, mechanical measurements showed that formin-generated filaments were the main
determinant of actin-based cortical elasticity. Our computer simulations showed that cells could control the length of cortical actin filaments independently of their turnover kinetics. Because filament length distribution likely affects cortical mechanics, this suggests that cells can respond to external stimuli by adapting their mechanical properties without affecting their response time.

RESULTS

To quantify cortical actin assembly kinetics, we used a combination of experiments and stochastic simulations. We first used fluorescence single-molecule (FSM) microscopy (26, 27) on formins and actin monomers. From the measured displacements and lifetimes, we inferred the values of molecular assembly and disassembly rates through fitting of analytical functions describing single-molecule kinetics and by comparison to stochastic simulations of single filaments. Finally, we used data from FRAP experiments in combination with stochastic simulations of a finite part of the cell cortex to determine relative protein abundances.

Formin kinetics assessed by FSM

We started by characterizing the filament elongation kinetics of the formin Diaph1 in steady-state cortices of cervical cancer HeLa cells and in blebbing melanoma M2 cells. In the latter case, we only considered cortical regions outside of blebs. We chose these two cell lines because they are from very different origins and the proteic composition and ultrastructural organization of their cortices are well characterized (19, 28, 29). Recent work has, in particular, shown that in these cells, actin filaments of the submembranous cortex are nucleated primarily by the Arp2/3 complex and the formin Diaph1 (19).

After being activated at the membrane, formins nucleate actin filaments and remain attached to their barbed ends, where they assist subsequent elongation (17, 30, 31). When imaged with single-molecule techniques, individual formins bound to growing barbed ends can be tracked (30). In contrast, proteins not bound to an actin filament diffuse so fast that they cannot be tracked and only contribute to background fluorescence (26). We used high–numerical aperture (NA) spinning disc confocal imaging to follow single molecules in an equatorial focal plane midway through the cell, where the cortical actin network is approximately isotropic and perpendicular to the plane of focus (fig. S1, A to C, and sections SI and SIIB). Alternative methods, such as total internal reflection fluorescence microscopy, are limited to the basal plane, where cells form stress fibers and focal adhesion in addition to cortex, making data analysis very challenging (fig. S1C). When we expressed Diaph1-GFP (green fluorescent protein) at low levels using truncated cytomegalovirus (CMV) promoters (26) and imaged cells, we could observe individual fluorescent particles moving in the plane of the cortex over several hundreds of nanometers (Fig. 1A and movies S1 to S3).

First, we ascertained that these represented single fluorescent molecules by verifying that they photobleached in a single step (fig. S2A). To increase the number of observable single molecules per cell, we absolved ourselves from the biochemical processes of formin activation by expressing a constitutively active Diaph1 (CA-Diaph1-GFP) (Fig. 1A). In contrast to Diaph1, CA-Diaph1 molecules are active without binding RhoA (32). We recorded the fluorescence intensity along the cortical layer and tracked the positions of local maxima over time (Fig. 1B), restricting our analysis to molecules that appeared and disappeared during our observation. The distribution of CA-Diaph1-GFP lifetimes was exponential, with a detachment rate $\omega_{\text{off}} = 0.12 \pm 0.1 \text{ s}^{-1}$ [Table 1 and fig. S3A, consistent with the studies by Kovar et al. (17) and Romero et al. (33)]. The lifetime distribution of full-length Diaph1 was not significantly different, with a detachment rate $\omega_{\text{off}} = 0.12 \pm 0.1 \text{ s}^{-1}$ ($P = 0.9$), indicating that CA-Diaph1-GFP protein dynamics were representative of active cortex-associated Diaph1-GFP (fig. S3B).

Because of constitutive activation, we expected that all traceable CA-Diaph1-GFP molecules should represent proteins engaged in filament elongation. However, overall, only 75% of molecules moved directionally along the cortical layer (Fig. 1, B and B2), whereas the rest appeared immobile (Fig. 1, B and B1). To understand the origin of this immobile fraction, let us first note that our setup recorded projections into the focal plane of the molecule displacements (Fig. 1C). Whenever the recorded travel distances were smaller than our spatial resolution (pixel size, 133 nm), the particle appeared immobile (Fig. 1C). For an isotropic cortex, geometric and kinematic considerations show that 20 to 30% of molecules should appear immobile in our setup (section SIIB and fig. S5), matching the observed fraction of immobile molecules. We conclude that all observed molecules were moving but, because of the projection of trajectories into the focal plane, a portion appeared immobile. Note that fluorescent molecules can leave the focal volume, and this introduces an error of less than 5% (Supplementary Materials).

We then sought to infer the rate of formin-mediated filament elongation from the trajectories of single molecules. The displacements could result from the filament elongation activity of CA-Diaph1-GFP (30), the activity of molecular motors inducing cortical flows (34), thermal noise (27), or a combination of these. To collectively quantify the contributions from processes other than CA-Diaph1-GFP–induced polymerization, we incubated cells with the formin inhibitor SMIFH2 that prevents monomer addition to formin-capped filaments (35). SMIFH2 almost completely suppressed CA-Diaph1-GFP motility (Fig. 1E, inset, gray line). In contrast, inhibition of myosin II motor proteins by treatment with the Rho-kinase inhibitor Y27632 showed no visible impact on Diaph1 motility compared to control cells (Fig. 1E, inset, blue line). If thermal noise contributed significantly to the observed movement of Diaph1 molecules, the superposition of the distributions obtained from the SMIFH2 and Y27632 data should contain the contribution of thermal noise to both distributions. This can be done by a convolution of the respective experimental distributions (section SIIC). There is no significant deviation of the measured distribution under control conditions from the convolution of distributions in the presence of SMIFH2 and Y27632, respectively (Fig. 1E). We concluded that Diaph1 movement was mainly due to formin-mediated polymerization alone (Fig. 1E and section SIIC).

The recorded displacements did not appear to have a preferred direction of motion, confirming isotropy of filament orientation in the cortical plane. Furthermore, trajectories were straight, consistent with electron micrographs (Fig. 1D) (36). For a constant filament elongation rate and exponentially distributed binding times, the distribution of displacements should be exponential. Indeed, the distribution of projected displacements inferred from an exponential distribution of displacements in 3D for an isotropic cortex accurately fits the measured distribution (Fig. 1E and eq. S14). From the fit, we obtained that, in HeLa cells, CA-Diaph1-GFP molecules polymerized, on average, 20 to 30% of molecules should appear immobile in our setup (section SIIB and fig. S5), matching the observed fraction of immobile molecules. We conclude that all observed molecules were moving but, because of the projection of trajectories into the focal plane, a portion appeared immobile. Note that fluorescent molecules can leave the focal volume, and this introduces an error of less than 5% (Supplementary Materials).

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the equivalent of a 3900-nm-long filament before detaching (M2 cells: 2500 nm).

Knowledge of the distribution of polymerized lengths, together with the formin detachment rate $\omega_{\text{off,F}}$, allowed computation of the rate $k_{\text{on,F}}$ of formin-assisted subunit addition to barbed ends (eq. S13). To this end, we calculated the distribution of travel distances expected for constant rates $\omega_{\text{off,F}}$ and $k_{\text{on,F}}$, and then fitted the resulting expression to the experimental distribution using $k_{\text{on,F}}$ as a free parameter (Fig. 1E, black lines and circles). This yielded $k_{\text{on,F}} = 136$ subunits per second (sub/s) for HeLa cells and $k_{\text{on,F}} = 102$ sub/s for M2 cells (Fig. 1E), comparable to values measured in vitro (17, 32). As an independent control, we also determined $k_{\text{on,F}}$ directly from the distribution of the
molecule velocities with the caveat that the data are much more noisy, and obtained $k_{\text{on,F}} = 140$ sub/s (M2 cells: $k_{\text{on,F}} = 100$ sub/s), consistent with the previous values.

### Growth kinetics of Arp2/3-nucleated filaments by FSM of actin monomers

Next, we sought to quantify the growth kinetics of filaments due to monomer addition at free barbed ends to estimate the length of filaments nucleated by Arp2/3. This information cannot be obtained from tracking Arp2/3 complexes because they nucleate actin filaments at their pointed end, where they block monomer removal. Instead, we measured the lifetime and trajectories of single actin-GFP molecules, reporting on individual actin monomers within filaments (Fig. 2 and section S1B). Their large number led to a higher background signal than in the case of formins (Fig. 2A), but we were still able to track individual molecules. In contrast to the tracks of single formins, the trajectories of single actin protomers do not contain information about actin filament assembly, and thus, we did not analyze their distribution. However, consistent with what we found for formin-nucleated filaments, we found that myosin contractility did not appear to participate in protomer motion (see Fig. S6B). In contrast to CA-Diaph1-GFP (Fig. S3A and B), the distribution of actin-GFP molecule lifetimes presented two distinct characteristic time scales, indicative of the two subpopulations of actin filaments previously reported to coexist in the cortex (Fig. 2B, inset) (18). Consistent with this, one of these subpopulations disappeared upon treatment with SMIFH2, indicating that they were nucleated by Diaph1 (Fig. 2C), whereas the other disappeared upon inhibition of the Arp2/3 complex with CK666 (Fig. 2D) (37, 38), consistent with the studies by Fritzsch et al. (18) and Bovellan et al. (19).

The growth kinetics at free barbed ends cannot be directly inferred from the actin lifetime distributions. However, we can infer these rates by making assumptions about the underlying molecular mechanisms, and fit the corresponding predicted lifetime distributions to the data. To this end, we used mean-field theories and stochastic simulations of single filaments (section SIII). Because the molecular processes of depolymerization and severing, have yet to be characterized in detail in vitro and in vivo (39–43), we decided to describe actin filament disassembly by using an effective disassembly rate $k_{\text{off}}$ that comprises the effects of all depolymerization mechanisms, including end-depolymerization and severing.

Explicitly, we considered growth at the barbed end and shrinkage at the pointed end. Barbed ends grow at a rate $k_{\text{on,F}}$ if formin is bound and at rate $k_{\text{on,0}}$ otherwise. Filaments shrink at rate $k_{\text{off}}$ unless capped by an Arp2/3 complex (Fig. 2E). Formin detaches from filaments at a rate $\omega_{\text{off,F}}$ and Arp2/3 at a rate $\omega_{\text{off,A}}$. We will see below that this implies that filaments grow on average as long as the nucleator is bound and shrink after it has been released.

At this point, three unknown parameters remain: $k_{\text{off}}, k_{\text{on,0}}$, and $\omega_{\text{off,A}}$. First, we determined the Arp2/3 release rate $\omega_{\text{off,A}}$ from the distribution of actin lifetimes in cells treated with SMIFH2. In this case, only one characteristic time scale remained that equals $1/\omega_{\text{off,A}}$ (Fig. 2C and section SIIIA). Similarly, after treatment with CK666, only one subpopulation remained, allowing us to obtain $k_{\text{off}}$ (Fig. 2D, section SIIIB).

The remaining unknown parameter $k_{\text{on,0}}$ can be determined by fitting the initial peak of the lifetime distribution in the presence of SMIFH2 (Fig. 2C). To this end, we performed stochastic simulations of single filaments (Materials and Methods and section SIIIC) to reproduce the peak value of experimental curves. Single-filament simulations using this value of $k_{\text{on,0}}$ yield lifetime distributions consistent with those measured in the presence of CK666 and under control conditions (Fig. 2, B and D). Explicitly, our simulation predicted $k_{\text{on,0}} = 28$ sub/s (M2: $k_{\text{on,0}} = 21$ sub/s), $k_{\text{off}} = 29$ sub/s (M2: $k_{\text{off}} = 23$ sub/s), and $\omega_{\text{off,A}} = 0.23$ s$^{-1}$ (M2: $\omega_{\text{off,A}} = 1.1$ s$^{-1}$). These values are comparable to results from in vitro experiments (Table 1). Knowledge of the formin- and Arp2/3-mediated nucleation rates is not needed for obtaining the kinetic parameters because these rates affect filament abundance rather than turnover time scales.

The actin turnover processes considered above imply an exponential distribution for the length of formin- and Arp2/3-nucleated filaments. Having obtained a full parametrization of actin turnover processes, we can use the simulations to calculate the average filament lengths. In HeLa cells, we calculated that formin-nucleated filaments had an average length of 1200 nm, whereas the average length of Arp2/3-nucleated filaments was 120 nm (M2 cells: 60 and 600 nm; Fig. 3A, full lines). The latter was consistent with results from electron tomography (44) and numerical simulations of the lamellipodium (45), as well as with theoretical predictions based on the movement of single proteins at the cell surface (34, 45). We found overall shorter lengths in the blebbing melanoma cells that have a less stable cortex (Table 2). In our experiments, in both cell types, we found that 20 to 25% of the total protomers in F-actin (18) were incorporated in filaments nucleated by formins and the remainder in filaments nucleated by Arp2/3 (Table 2). As a consequence, shorter filaments are more abundant than longer ones. Consistent with this finding, scanning electron micrographs of the cortex of wild-type HeLa cells show the presence of both long and short filaments, with the former being visibly less abundant (Fig. 3B). Treatment with the formin inhibitor SMIFH2 appeared to lead to a decrease in long filaments, and treatment with CK666 appeared to lead to a decrease in short filaments (Fig. 3B), consistent with the studies by Bovellan et al. (19) and Eghiaian et al. (46).

### Table 1. Summary of parameters of filament growth kinetics inferred from FSM experiments and single-molecule simulations compared with values in vitro from the literature for CA-Diaph1 and actin molecules.

| Experiment | HeLa cells in vivo | M2 cells in vivo | Reported values in vitro | Source |
|------------|-------------------|------------------|--------------------------|-------|
| $k_{\text{on,F}}$ (sub/s) | 136 ± 14 | 102 ± 10 | 46.9 × $c^T$ | (17) |
| $k_{\text{on,0}}$ (sub/s) | 28 ± 2 | 21 ± 2 | 11.6, 6.5–9.5, 9.1–10.9 × $c^T$ | (17, 33, 66) |
| $\omega_{\text{off,F}}$ (1/s) | 0.12 ± 0.02 | 0.15 ± 0.02 | 1.23 | (47) |
| $\omega_{\text{off,A}}$ (1/s) | 0.23 ± 0.02 | 1.1 ± 0.1 | 6.25–20, 4.7–51.6 | (66, 69, 70) |
| $k_{\text{off}}$ (1/s) | 29 ± 3 | 23 ± 2 | | |

In the fourth column, $c^T$ is the concentration of ATP-actin.
Stochastic simulations of the homeostatic actin cortex

Our quantitative analysis of molecular cortical actin turnover revealed clear differences in the kinetics of turnover of filaments nucleated by formins and by Arp2/3. Previously, FRAP experiments on cortical actin turnover had suggested the existence of two kinetically distinct filament subpopulations representing relative fractions $f_1$ and $f_2$ of the total number of actin protomers bound in filaments whose fluorescence recovered with the rates $w_{d,1}$ and $w_{d,2}$ (18). Thus, we wanted to check whether the processes considered above can reproduce these FRAP experiments.

We set up stochastic simulations of cortical actin turnover in a finite volume that comprised the processes described above, as well as actin nucleation by Diaph1 and the Arp2/3 complex at molecular rates $n_F$ and $n_A$, respectively (Materials and Methods). The finite cortex simulations also consider explicitly the concentration $c_{act}$ of free globular actin (G-actin), the concentration of Diaph1 $c_{form}$, and the concentration of Arp2/3 complexes $c_{arp}$, such that we have a closed description of cortical actin turnover. The total rate of actin assembly is then a function of the molecular rates determined above, as well as the G-actin concentration and the concentration of free barbed ends (Materials and Methods). The simulations thus contain three new a priori unknown parameters: $n_{off,A}$, $n_{off,F}$, and $c_{act}$.

From the FRAP experiments, we obtained three quantities that we could compare with the simulation results: the fraction of Arp2/3- to formin-generated filaments ($f_1/f_2$) and the rates of fluorescence recovery of the two subpopulations ($w_{d,1}$ and $w_{d,2}$), which were determined by fitting a weighted sum of two exponentials to the FRAP data (18). We...
found that the finite cortex simulations of a FRAP experiment, where a circular region of 1-μm radius was bleached within a total area of 26.6 × 26.6 μm² (Fig. 3C and movie S4), reproduced the functional form of fluorescence recovery obtained from the experiments (Fig. 3D). The fits of the simulation data to the experimental curves yielded $c_{\text{act}} = 3 ± 0.01$ μM, $c_{\text{arp}} = 24 ± 0.01$ nM, and $c_{\text{form}} = 0.2 ± 0.04$ nM (M2: $c_{\text{act}} = 2.5 ± 0.01$ μM, $c_{\text{arp}} = 24 ± 0.04$ nM, $c_{\text{form}} = 0.17 ± 0.04$ nM) (table S1). These values are consistent with in vitro experiments (47, 48).

The finite cortex simulations also allow computation of the filament length distribution of both subpopulations. These agree well with the distributions inferred above (Fig. 3A, triangles and circles) and show that our analysis of actin turnover is inherently consistent. We then used the simulations to study the effects of parameter changes on the homeostatic cortex (Fig. 4), where we focused on parameters that cells are known to control. Most G-actin in cells is sequestered by proteins such as thymosin-β4; as a consequence, cells can rapidly mobilize a large pool of G-actin by releasing sequestration. An increase of the total actin concentration led to a lengthening of the filaments of both populations (Fig. 4A), consistent with experimental results obtained for formins in cells (49). Remarkably, though, the
turnover times of the actin filament subpopulations, as quantified by $1/w_{d,1}$ and $1/w_{d,2}$, were not significantly affected by filament lengthening (Fig. 4B). Thus, cells can adapt their structural and mechanical properties without affecting their response time to external signals. Conversely, signaling can modulate the time that an individual nucleator is bound to an actin filament, an effect identical to changing the off-rate $w_{off,F}$ or $w_{off,A}$ for Diaph1 or the Arp2/3 complex, in our finite cortex simulations. In both cases, the length distribution of the filament subpopulation whose nucleator was not being regulated was unaffected. The turnover time of the filaments whose nucleator was being regulated ($1/w_{d,i}$) decreased with increasing nucleator off-rate (Fig. 4, C to F), but the turnover time of the other population was unaffected. Thus, the two subpopulations can be regulated independently from one another in length and turnover rate. The relative abundances $f_1$ and $f_2$ of filaments in the two subpopulations changed in response to changes of the respective nucleator concentrations (fig. S4), suggesting a mechanism by which cells could change their cortical mechanical properties by altering the activity of each nucleator independently.

Next, we investigated whether severing alone might generate two subpopulations of F-actin with different lengths in the cortex in the presence of only one filament nucleation pathway. Using the finite cortex simulations, we found that, in the presence of a single-filament subpopulation, severing leads to the generation of a cortex whose fluorescence recovers with multiple relaxation times rather than two distinct time scales, as is the case when two distinct nucleation pathways are present (section SV).

**Atomic force microscopy measurements of actin cortex elasticity**

In light of the significant differences in filament length and abundance of the two cortical filament subpopulations, we asked how each subpopulation contributed to cortical mechanical properties. We characterized cortex elasticity with atomic force microscopy (AFM), using shallow indentations (100 to 500 nm) and small contact areas ($\mu$m$^2$) to minimize contributions from the cytoplasm (Fig. 5, A and B). Recent experimental and theoretical work indicates that, under these conditions,
the measured stiffness is dominated by the macroscale mechanical properties of the cortex (50). Cortical elasticity measurements yielded an elastic modulus of $E = 4.0 \pm 1.5$ kPa in HeLa cells ($N = 199$ curves, $n = 28$ cells). Previous work has indicated that Arp2/3 inhibition with 100 μM CK666 leads to a ~30% reduction of cortical actin protomers incorporated in filaments (19), but this did not result in a significant reduction of cortical elasticity ($E = 3.5 \pm 1.5$ kPa, $P = 0.1$, $N = 169$ curves on $n = 23$ cells). In contrast, inhibition of formin with 40 μM of the inhibitor SMIFH2 resulted in a significant decrease of ~25% of the elastic modulus ($E = 3.0 \pm 1.7$ kPa, $P < 0.01$, $N = 210$ curves, $n = 30$ cells, Fig. 5C), despite previous reports showing that Diaph1 depletion only reduces cortical actin protomers by ~15% (19). When cortical turnover was completely blocked by perturbing both filament populations simultaneously with the same concentrations of SMIFH2 and CK666 as above (18), this resulted in a marked ~50% decrease of cortical elasticity ($E = 2.0 \pm 1.1$ kPa, $N = 201$ curves, $n = 29$ cells, Fig. 5C). This value is consistent with the cortical elasticity measured after complete actin cortex depolymerization by application of 5 μM cytochalasin D (51). Our results therefore suggest that both short and long filaments contribute to cortical elasticity but that the longer formin-nucleated filaments are a stronger determinant of the macroscale cortex mechanical properties. The differential effect of perturbation of long or short filaments on elasticity could be due either to architectural features of the actin cortex or to differences in the actin-binding proteins recruited by each filament subpopulation (52).

**DISCUSSION**

Together, our experimental and computational results paint the following picture of cortical actin homeostasis. For actin filaments not bound to nucleators, monomeric actin is incorporated at the barbed ends of actin filaments and lost through disassembly, which includes the dissociation of monomers from pointed ends as well as severing that can potentially lead to the formation of small actin oligomers. Because the effective disassembly rate exceeds the assembly rate for these filaments, this results, on average, in a loss of actin monomers and eventual filament disappearance. The amount of cortical F-actin is kept constant through the action of two main actin-nucleating factors: Diaph1, which speeds up growth at the barbed end, and the Arp2/3 complex, which prevents actin disassembly from the pointed end. Our results suggest that other processes contribute less than 10% to cortical actin turnover, consistent with previous work showing that Diaph1 and Arp2/3 are the main contributors to cortical actin assembly (19). Filaments nucleated by either pathway differ significantly in abundance, length, and turnover kinetics. Formin-nucleated filaments make up only 10% of the total number of cortical filaments, but because they are, on average, 10 times longer than Arp2/3-nucleated filaments, they still account for 20 to 25% of the total actin protomers bound in actin filaments (section SVI). Their long length results in a turnover rate that is roughly 20 times smaller than that of Arp2/3-nucleated filaments.

Whereas the formin associated rates $\omega_{\text{eff},F}$ and $k_{\text{on},F}$ could be directly inferred from single-molecule formin measurements, quantification of the elongation rate of free barbed ends $k_{\text{on},0}$, of the lifetime of Arp2/3 at pointed ends $\omega_{\text{eff},A}$, and of actin filament disassembly $k_{\text{off}}$ required assumptions about the underlying molecular processes. Consequently, these values are tied to the dynamics of the assumed molecular mechanisms. Notably, filament disassembly is more complex than the sequential removal of actin protomers from pointed ends (21, 39–43). Moreover, it is possible that the disassembly process and kinetics are different in formin- and Arp2/3-nucleated filaments. In particular, for Arp2/3-nucleated filaments, the pointed-end depolymerization rate $k_{\text{off}}$ could be nonzero, which would, on average,
reduce the length of Arp2/3-nucleated F-actin. However, a comprehensive detailed molecular picture of actin filament depolymerization in cells is currently not available, such that we decided to describe filament disassembly by an effective disassembly rate resulting from all of the depolymerization processes acting concurrently on the filaments in the cell. On the basis of stochastic simulations that explicitly incorporate filament severing, we do not expect significant changes in the average filament length distributions if a more detailed scheme for filament disassembly is assumed. Our conclusions about the possible separate control of cortical filament length and cortical turnover time, and about the possible mechanical implications of filament turnover on cortex elasticity, should remain unaffected by our assumptions on the filament disassembly process.

On the basis of our work, distinct functions can be attributed to the two filament populations. The kinetics and length of formin-generated filaments suggest that they ensure cortex integrity. Consistent with this, cortical elasticity is strongly affected by perturbation of the formin-nucleated filaments, as shown by our AFM measurements. In contrast, the Arp2/3-nucleated filaments do not appear to play an important role in cortical mechanics despite their higher abundance. Thus, they may be involved in the generation of cell protrusions (53) or exocytosis and endocytosis (54), and constitute a rapid reaction process for cells to respond to extracellular signals (55). We can further speculate that the extensive blebbing observed in M2 cells might be a consequence of the overall shorter length of cortical actin filaments in these cells, something that might compromise the structural integrity of the cortex, whereas a moderate increase of the average length by a factor of roughly 2 suffices to stabilize the cortex of HeLa cells (56).

From a mechanical point of view, the very different average length of the actin filaments in each subpopulation, together with their different effect on cortical mechanics, suggests that the longer formin-nucleated filaments may distribute stresses over length scales of several micrometers, whereas the shorter and more dynamic Arp2/3-nucleated filaments contribute little. This is consistent with the truss bridge model of the actin cortex (57) in which tightly connected short filaments construct the cortical meshwork and respond to fast localized perturbations in the range of the cortex thickness ~100 nm. In contrast, the long fibers that are mostly under tension provide mechanical integrity to the cell by spreading applied forces over length scales comparable to the size of the cell. Furthermore, our results are consistent with computational simulations that indicate that a small portion of longer filaments can significantly increase the elasticity of filament networks (58).

One intriguing prediction of our finite cortex simulations is that actin turnover time can be controlled independently of filament length (Fig. 4, A and B). This may allow cells to adapt the structural organization of their cortex and its mechanical properties without compromising their response time to external signals. Furthermore, our simulations indicate that changes in the relative activities of each type of nucleator will alter the length distribution of filaments (Fig. 4, C to F). Together with our mechanical measurements, this suggests that changes in nucleator activity downstream of biochemical signaling represent an important regulation pathway for cells to adjust their mechanical properties. Further quantification of in vivo kinetic rates will be essential for a molecular characterization of actin behavior and dynamics in response to signaling, mechanical stimulation, or during the cell cycle.

**MATERIALS AND METHODS**

Cell culture

HeLa cells and filamin-deficient M2 melanoma cells (59) were cultured at 37°C in an atmosphere of 5% CO₂ in air. M2 cells were kept in minimum essential medium (Life Technologies) with penicillin/streptomycin, glutamine, and 10% of an 80:20 mix of newborn calf serum/fetal bovine serum (FBS). HeLa cells were cultured in Dulbecco’s modified Eagle’s medium (PAA or Gibco) with penicillin/streptomycin, L-glutamine, and 10% FBS. For experimentation, cells were trypsinized and plated onto 25-mm-diameter glass coverslips and cultured overnight. Imaging was done in Leibovitz L15 medium (Life Technologies) supplemented with 10% FBS.

Cell lines, transfections, and transductions

For FRAP experiments, actin-GFP stable cell lines were created using retroviruses generated by transfecting 293-GPG packaging cell lines (a gift from D. Ory, University of Washington) with the gene of interest inserted into the pRetroQ-Ac-GFP vector (Clontech). Cells were then selected with puromycin and subcloned as described by Charras et al. (28). For single-molecule imaging, the CMV promoter of Diaph1-GFP, CA-Diaph1-GFP, and actin-GFP was replaced with a truncated minimal CMV promoter described by Watanabe and Mitchison (26) and referred to as ΔCMV in the following. To study the effects of pointed-end severing, cells expressed dominant-negative cofilinS3E-cherry in addition to CMV-truncated actin-GFP. Cells were transfected using Lipofectamine 2000 (Life Technologies) according to the manufacturer’s protocol, using 1 μg of complementary DNA per well of a six-well plate.

Drug treatments

SMIFH2, CK666, and Y27632 were purchased from Merck Biosciences. Drugs were added to the culture medium at the desired concentration, and the cells were left to incubate for at least 10 min before imaging. Inhibitors were also present at the same concentration in the imaging medium.

Confocal microscopy

All FRAP experiments were done using a 1.3 NA 100× oil immersion objective on a scanning laser confocal microscope (FluoView FV1000, Olympus) at 37°C (see fig. S1). For imaging GFP on the scanning confocal microscope, laser intensities between 1 and 5% of a 20-mW laser were used to both obtain a strong signal and minimize photo-bleaching due to image acquisition. Images were acquired at 0.1- to 1-s intervals to minimize the general loss of fluorescence due to imaging while still sampling recovery sufficiently fast to capture the recovery kinetics of the protein of interest.

Single-molecule experiments were effected using a high-NA (NA = 1.3) 100× oil immersion objective on an inverted microscope (IX81, Olympus) fitted with a spinning disc head (CSU22, Yokogawa) coupled to an Andor iXon electron-multiplying charge-coupled device camera. Fluorophores were excited at 488-nm wavelength for GFP-tagged proteins and at 543-nm wavelength for RFP (red fluorescent protein)–tagged proteins. Laser intensities of 100% of a 20-mW laser were used to obtain a strong fluorescence signal. Images were acquired at 0.35- to 5-s intervals, with a 350-ms integration time averaged over 2 frames for 30 frames in total. Images were analyzed using MATLAB (MathWorks Inc.) and ImageJ (http://rsbweb.nih.gov/ij/).
Atomic force microscopy

AFM nanoindentation tests were performed with a JPK NanoWizard I (JPK Instruments) interfaced to an inverted optical microscope (IX81, Olympus). For our measurements, we used cantilevers with small pyramidal tips (MLCT, Bruker; nominal spring constants of 0.07 N m$^{-1}$). Analysis of force indentations was restricted to depths of 100 to 500 nm (leading to forces less than 200 pN) to maximize the contribution of cortex stiffness to cantilever deflection, enabling us to probe cell cortex elasticity while minimizing contributions from the cytoplasm (50, 60).

Cantilever actual spring constants were determined using the thermal noise method implemented in the AFM software (JPK SPM). Before indentation tests, the sensitivity of the cantilever was set by measuring the slope of force-distance curves acquired on glass regions of the petri dish. With the optical microscope, the tip of the cantilever was aligned over regions above the cell nucleus, and a couple of indentation measurements were performed on the cytoplasm. Force-distance curves were acquired with an approach speed of 5 μm s$^{-1}$ until reaching the maximum set force of 400 pN. The tip velocity used during indentation tests was chosen such that cantilever indentation times were shorter than filament turnover times and longer than poroelastic time scales (61). The considered range of indentation depths was comparable to both the lengths of the small Arp2/3 and large formin-nucleated actin filaments, and therefore enabled us to detect the contribution of both networks. Using the method described by Lin et al. (62), we found the contact point, and subsequently, we calculated the indentation depth δ by subtracting the cantilever deflection d from the piezo translation z after contact (δ = z − d). The elastic moduli were extracted from the force-distance curves by fitting the contact portion of curves to a Hertz contact model between a pyramid and an infinite half-space (63).

FRAP protocol

In FRAP experiments, a small circular region of interest (r = 2 μm) centered on part of the cell cortex was imaged, as described by Fritzsche et al. (18) and Fritzsche and Charras (64). In the center of this region of interest, a smaller circular bleaching region (r = 1 μm) containing both cortex and cytoplasm was chosen. This choice of imaging and bleaching region helped to minimize acquisition-induced fluorescence loss by not exposing the whole cell volume to light. After photobleaching, fluorescence recovery was followed separately in the cortex and the cytoplasm by segmenting these areas on the basis of prebleach images.

To assess the fluorescence loss due to imaging-induced photobleaching, fluorescence from a cortical region separated from the bleached region was simultaneously recorded. Bleaching was performed by scanning the 488-nm beam operating at 100% laser power over a circular bleach region with a 500-nm radius. The experimental protocol was as follows: Five frames were acquired for normalization of the fluorescence signal. Bleaching was carried out with one single iteration of the laser pulse at 8 μs/pixel. Finally, recovery was monitored over 100 frames. Frames were separated by either 100 ms or 1 s, depending on the recovery kinetics of the protein of interest.

FSM protocol

To exclusively consider cortical F-actin dynamics, single molecules were monitored in an optical section located midway through the cell height (fig. S1B, equatorial plane), where a well-defined cortex is present. Measurements could not be performed in the cortex at the basal or apical side of the cells (fig. S1, B and C) because F-actin was mainly present in the form of stress fibers (fig. S1C, basal plane) or microvilli, respectively (fig. S1C, apical plane).

In practice, molecule motility was monitored in a 300-nm-wide strip around the cell periphery corresponding to the cell cortex. For single molecules to be detected within the imaging region, they needed to have residence times longer than the integration time within the volume of the point spread function (27, 62, 65).

In contrast, proteins diffusing freely in the cytoplasm only contribute weakly to the fluorescence signal at any given position. Similarly, proteins freely diffusing in the membrane, such as a CA-Diaph1 protein not bound to the actin cortex, only contribute membranous background signal. The homogeneous background signal stemming from rapidly diffusing proteins has a significantly lower intensity than the signal emanating from proteins that are immobile over the time frame of image acquisition (26). For example, G-actin monomers freely diffusing in cells have an effective diffusion constant of $D_{act} \approx 25 \mu m^2/s$ (18), and thus travel approximately 40 pixels (or ∼5 μm) in 1 s.

The experimental protocol was as follows: acquisition at 0.5- to 5-s intervals for capturing actin monomers bound to the cortex only, and 200- to 400-ms illumination of each individual frame averaging each time point over two frames, giving a total integration time of 400 to 800 ms. The total number of frames acquired was 15 to 30 for each cell examined.

Simulation algorithm for single-filament simulations

Stochastic simulations were done following a Gillespie scheme in C/C++ using the implementation of the Mersenne Twister random number generator from the boost libraries. We call them single-filament simulations.

The filament is represented by a linear array of varying length, storing the time of addition of each protomer. In the case of Arp2/3 nucleation, a filament is initiated as a single monomer, and the pointed end is considered capped by the Arp2/3 complex. Protomers are added to the barbed end at constant rate $k_{on,0}$. Protomer release from the pointed end occurs at a rate $k_{off}$ and starts after a randomly chosen time corresponding to the time when the Arp2/3 molecule is released. The single-filament simulation stops when the last protomer is removed, and a histogram of the protomer lifetimes is generated. The analysis of formin-nucleated filaments follows the same lines. Protomers are added at the barbed end at a rate $k_{on,0}$ up to a randomly chosen time corresponding to formin release. After release, protomers are added at rate $k_{on,0}$. Protomer release at the pointed end occurs at a constant rate $k_{off}$ throughout the simulation. In both cases, the distribution of lifetimes was obtained from 1000 independent runs of the single-filament simulation.

Fitting procedures

To obtain the values of the various kinetic rates of actin assembly and nucleator release rates, we fitted the solution of our analytical and computational models to the measured distributions. These distributions displayed a maximum at a finite time and a subsequent exponential decay. First, we used the analytical expressions eqs. S23 and S28, respectively, to fit the exponential long-time behavior. To also capture the initial peak, we then used stochastic single-filament simulations, which depend on more parameters. Fits were done using a log-likelihood method.
Simulation algorithm for finite cortex simulations
Stochastic simulations of the cortex were done following a Gillespie scheme implemented in C/C++, which we call finite cortex simulations. Each cortical filament is represented by a linear array of varying length. Simulations are carried out with the same molecular dynamics as described above for the single-filament simulations. In addition, we distinguish between fluorescing and nonfluorescing monomers. The number of filaments varies through nucleation and complete depolymerization. The total numbers $N_{\text{1ot}}$ of actin monomers, $N_{\text{form}}$ of formins, and $N_{\text{arp}}$ of arp2/3 complexes are fixed. Monomers are added to free barbed ends at a rate $k_{\text{on,b}} = r_{\text{on,b}} \, \Gamma_{\text{act}}$, with $\Gamma_{\text{act}}$ being the current free monomer concentration. Monomers are added to barbed ends bound to a formin at rate $k_{\text{on,F}} = r_{\text{on,F}} \, \Gamma_{\text{act}}$. Because of the large diffusion constant of free G-actin monomers, their concentration is homogeneous in a simulated volume of 50 $\mu$m$^3$. We considered Arp2/3 complexes to be single entities and did not distinguish their subunits. Similarly, formin dimers were taken to be single molecules. When released, nucleators instantaneously generated new filaments.

The cortex is represented on a 2D grid of $200 \times 200$ pixels, corresponding to the image obtained on the experimental setup. Each pixel had a width of 133 nm. We chose periodic boundary conditions for our simulations to reflect the fact that the cell is many fold larger than the bleached zone. In the cortical region, filaments are represented as planar curves. The effective length added by incorporation of a single monomer into a filament is 2.7 nm, corresponding to one-half of its radius. To mimic the finite persistence length of the filaments, the orientation of a newly added monomer is chosen from a normal distribution with a variance of 0.02 and a mean equal to the orientation of the previous monomer (movie S4).

Finite cortex simulations were first run until the system reached steady state. After a time of the order of $T_{\text{bleach}} = 10^3$ s, the system is “bleached” by marking all monomers inside filaments as non-fluorescent. Monomers that are subsequently incorporated into a filament are set to be fluorescent. The fluorescence within the bleached zone is given by the number of fluorescent monomers that have been incorporated into the filaments after time $T_{\text{bleach}}$. Parameter values are summarized in table S2.

SUPPLEMENTARY MATERIALS
Supplementary material for this article is available at http://advances.sciencemag.org/cgi/content/full/2/4/e1501337/DC1
section SI. Supplementary materials, methods, and figures
section SII. Determination of the formin-induced, barbed-end polymerization rate
section SIII. Single-filament computations to determine effective molecular rates
section SIV. Determination of filament length distribution in the subpopulations
section SV. Filament severing
section SVI. F-actin abundances in the actin cortex
fig. S1. Experimental setup.
fig. S2. Single-step photobleaching control by a temporal evolution of the molecule fluorescence intensity.
fig. S3. (A and B) Lifetime distribution with average lifetime $\tau_{\text{ave}} = 0.12 \pm 0.01$ of (A) Diaph1 (N = 1000 molecules) and of (B) CA-Diaph1 (N = 3000 molecules).
fig. S4. Actin filament fractions depend on the cortical nucleator concentrations.
fig. S5. Fraction $\Phi$ of immobile molecules as a function of the average filament length $\lambda$, according to eq. S5 with $p(\Phi) = \exp(-\Phi/\lambda)/\lambda$.
fig. S6. Effects on molecule mobility.
fig. S7. Illustration of monomer lifetimes during continuous filament growth.
fig. S8. Simulated FRAP curves for scenarios including filament severing.

table S1. Comparison between model parameters used in the finite cortex simulations and literature values.
table S2. Parameter values used in the simulations of FRAP experiments.
table S3. Parameter values for the two scenarios of filament severing.
movie S1. Fluorescence imaging of cortical Diaph1-GFP in a HeLa cell corresponding to Fig. 1A.
movie S2. Fluorescence imaging of cortical actin-GFP in an M2 cell.
movie S3. Detail of fluorescence imaging of cortical Diaph1-GFP in a HeLa cell corresponding to Fig. 1B.
movie S4. Cortex simulation of a FRAP/FLAP experiment in a HeLa cell.

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Acknowledgments: We wish to acknowledge the University College London Comprehensive Biomedical Research Centre for funding of microscopy equipment. Funding: M.F. was funded by a Human Frontier Science Program Young Investigator grant to G.C. (RGY 66/2013). E.M. is grateful for the financial support through a Wellcome Trust–Massachusetts Institute of Technology fellowship (grant WT103883). G.C. was supported by a University Research Fellowship from the Royal Society. C.E. and K.K. were supported by the Graduate School GK1276 and the SP81027 of the Deutsche Forschungs gemeinschaft. Author contributions: M.-F., G.C., and K.K. designed the research; M.F. performed experiments with help from G.C. and E.M.; C.E. developed and performed stochastic simulations; M.F., G.C., and K.K. wrote the manuscript with input from all authors; and all authors analyzed data. Competing interests: The authors declare that they have no competing financial interests. Data and materials availability: All data needed to evaluate the conclusions in the paper are present in the paper and/or the Supplementary Materials. Additional data related to this paper may be requested from the authors.

Submitted 27 September 2015
Accepted 30 March 2016
Published 22 April 2016

10.1126/sciadv.1501337

Citation: M. Fritzsche, C. Erenkämper, E. Moenendarbary, G. Charras, K. Kushe, Actin kinetics shapes cortical network structure and mechanics. Sci. Adv. 2, e1501337 (2016).
Actin kinetics shapes cortical network structure and mechanics
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Sci Adv 2 (4), e1501337.
DOI: 10.1126/sciadv.1501337