Electrochemical behavior of two austenitic stainless steel biomaterials

Comportamento eletroquímico de dois aços inoxidáveis austeníticos utilizados como biomateriais

Enrico J. Giordano
CCDM - Universidade Federal de São Carlos
E-mail: enrico@ccdm.ufscar.br

Neusa Alonso-Falleiros
EPUSP - Departamento de Engenharia Metalúrgica e Materiais
E-mail: neusa.alonso@poli.usp.br

Itamar Ferreira
FEM/UNICAMP - Departamento de Engenharia de Materiais
E-mail: itamar@fem.unicamp.br

Oscar Balancin
UFSCar - Departamento de Engenharia de Materiais
E-mail: balancin@ufscar.br

Resumo
O presente trabalho avaliou a resistência à corrosão localizada de dois aços inoxidáveis austeníticos utilizados na fabricação de implantes ortopédicos: o aço ASTM F138, material metálico atualmente mais utilizado em aplicações ortopédicas e o aço ISO 5832-9, aço com adição de nióbio e nitrogênio e que vem sendo apontado como uma alternativa para a substituição do aço F138, para aplicações mais severas de carregamento e tempo de permanência no interior do corpo humano. Ensaios de polarização mostraram que o aço ISO 5832-9 apresenta resistência à corrosão localizada muito superior à do aço F138. O potencial crítico de pite do aço ISO 5832-9 não foi observado na curva de polarização cíclica até o potencial de transpassividade do material. O ensaio potenciostático de corrosão por risco confirmou a superioridade do aço ISO 5832-9. Observou-se a reconstituição do filme passivo danificado mecanicamente, mesmo em potenciais tão elevados como 800 mV SCE. Análises por microscopia eletrônica de varredura confirmaram a presença de pites de corrosão de crescimento estável, na superfície da amostra de aço F 138, e a ausência desses pites, na amostra do aço ISO 5832-9. A maior resistência à corrosão localizada do aço ISO 5832-9 é, principalmente, atribuída ao aumento da estabilidade do filme passivo, sendo favorecida pela presença do nitrogênio em solução sólida intersticial, na austenita desse aço.

Palavras-chave: Biomateriais metálicos, corrosão localizada, aços inoxidáveis austeníticos, Fase Z, ISO 5832-9.

Abstract
Potentiodynamic and potentiostatic polarization measurements were conducted in 0.9% NaCl solution to investigate the localized corrosion susceptibility of two austenitic stainless steel biomaterials: a low nitrogen, according to ASTM F 138 - the metallic material most widely utilized today in orthopedic applications; and a nitrogen- and niobium-bearing stainless steel, according to ISO 5832-9, which has shown a promising potential as a substitute of the F138 steel for more severe loading applications and longer times inside the human body. The polarization tests revealed that the ISO 5832-9 steel is more corrosion resistant than the F138. The critical pitting potential of the ISO 5832-9 steel could not be observed in the cyclic polarization curve up to the value of potential corresponding to its transpassivity. The potentiostatic scratch test confirmed the superiority of the ISO 5832-9 steel, which heal the mechanically damaged passive film at applied potential as high as 800 mV (SCE). Scanning electron microscopy (SEM) examination confirmed the presence of corrosion pits - lacelike pits - in a stable growth stage on the surface of F 138 steel and the absence of such pits in the specimens of the ISO 5832-9.
The higher corrosion resistance of the latter is attributed to the increased stability of the passive film and the high tendency to repassivate, which, in turn, is favored by the presence of nitrogen in interstitial solid solution in the austenite of this type of steel.

**Keywords:** Austenitic stainless steel, localized corrosion, Z-phase, ISO 5832-9, metallic biomaterials, orthopedic implant.

## 1. Introduction

The deterioration of metallic implants in the human body is undesirable for two main reasons: the degradation process may impair the structural integrity of the implant and the products released through the degradation process may culminate in adverse biological reactions in the implanted patient. This deterioration may result, for instance, from the corrosion of the implanted metal. Corrosion of the implant surface may be uniform (general corrosion) or localized, affecting specific regions where the bodily fluids remain stagnated (crevice corrosion) or on localized random sites on the metal surface (pitting corrosion).

Moreover, the combination of the electrochemical corrosion process and of cyclic mechanical loads can, through the synergy corrosion-fatigue, accelerate the release of metallic particles (debris) and ions, leading to premature structural failure of the implant.

It is known that austenitic stainless steels owe their corrosion resistance to the formation of a superficial protective oxide film rich in Cr, named passive film, which, by adhering to the metal surface, acts as a kinetic barrier, inhibiting the corrosion process and keeping the release of ions at very low levels. Despite the high generalized corrosion resistance of this type of steel, they are susceptible to localized pitting or crevice corrosion.

For over ten years, the corrosion resistance of high nitrogen stainless steels has been the favorite topic of corrosion studies seeking to elucidate the role of nitrogen in the various processes: anodic dissolution; passivation; pitting corrosion; crevice corrosion and corrosion associated with mechanical loads (Sivakumar, Kamachi Mudali, Rajeswari, 1994; Levey and Van Bennekom, 1995; Rondelli, Vicentini, Cigada, 1995; Azuma, Miyuki, Kudo, 1996; Grabke, 1996; Jargelius-Pettersson, 1996; Kamachi Mudali et al., 1996; Rondelli, Vicentini, Cigada, 1997; Jargelius-Pettersson, 1999).

Small amounts of nitrogen suffice to promote significant variations in the mechanical and corrosion properties of the steels. The ISO 5832-9 steel, a nitrogen- and niobium-bearing austenitic stainless steel, has been indicated as an alternative to substitute F 138 steel, the metallic material most widely employed in orthopedics, for more severe loading applications and longer periods inside the human body, due to the combination of high strength, even in the annealed condition, associated with high localized corrosion resistance.

Although advantageous, the influence of some features of the ISO 5832-9 such as the presence of Z-phase - inherent phase in this type of austenitic stainless steel (Giordani et al., 2004) - on the corrosion resistance is not well understood.

This article reports on an evaluation, based on potentiodynamic and potentiostatic polarization tests, of the localized corrosion resistance, in an aqueous 0.9% NaCl solution, of two austenitic stainless steels used as biomaterials - F 138 and ISO 5832-9.

The effect of nitrogen on electrochemical behavior is also discussed, as are features of the corrosive attack investigated by SEM.

### 2. Materials and methods

The materials studied were the austenitic stainless steels ASTM F 138-97 and ISO 5832-9 (ASTM 1586), received as rolling bars with a 15.87 mm diameter (5/8"). Table 1 lists the chemical compositions of the steels.

All electrochemical tests were performed at least in triplicate in a 0.9% NaCl in de-ionized and distilled water solution at 22 ± 1°C for the two steels annealed at 1030°C for 1 hour. Before being embedded in polyester resin, the specimens were subjected to a surface passivation treatment in an aqueous solution of 20% HNO₃ at 35°C for 60 minutes, to prevent crevice corrosion at the metal/resin interface. The exposed transversal area, polished down to 1 μm with diamond paste, was approximately 1 cm². The potential was applied and the corrosion current recorded using a potentiostat (EG&G Princeton Applied Research, model 273A) coupled to a microcomputer. The reference electrode used was a saturated calomel electrode (SCE) and the counter electrode was of platinum. The specimens were immersed in the electrolyte one hour before the tests to reach a steady state potential.

The cyclic potentiodynamic polarization tests were conducted with a potential scan rate of 0.33 mV/s (1200 mV/h). The initial potential was -750 mV (SCE) and the potential sweep was reversed when the anodic current density reached 100 μA/cm². The cyclic polarization curves are presented following the conventions of the ASTM G3 standard and the terminology of the ASTM G15 standard.

The potentiostatic scratch test, initially proposed by Pessal and

| Material   | C   | Mn | Ni  | Cr  | Mo | N  | Nb | Fe |
|------------|-----|----|-----|-----|----|----|----|----|
| F 138      | 0.01| 1.7| 14.1| 17.4| 2.1| 0.04| —  | bal.|
| ISO 5832-9 | 0.02| 3.6| 10.6| 21.1| 2.4| 0.37| 0.42| bal.|
Liu (1971), is an alternative way to determine the critical pitting potential (Ec) of passivable metals. In this method the passive film is slightly damaged, here using an alumina tip, while the potential is applied by using the potentiostat which also records the corrosion current density developed before, during, and after scratching. The starting potential must be located in the passive region. If the damaged areas repassivate after the scratch, the current density drops to values near zero. Then, scratching is repeated at higher potential values (here using 20 mV steps) up to a potential value at which the damaged passive film does not repassivate, and the current density remains at high values or even increases with time. In this way, Ec is defined as the more noble value of potential above which the damaged film does not heal.

After testing, examinations on the exposed surface of the specimens were conducted in a scanning electron microscope (Jeol, model JSM-5900LV) to check the features of the corrosive attacks on the steels.

### 3. Results and discussion

Figure 1 shows representative cyclic potentiodynamic polarization curves of the F 138 and ISO 5832-9 steels. Table 2 lists the values of the parameters obtained from these tests. The electrochemical behavior displayed by F 138 steel was typical of materials presenting a well-defined critical pitting potential. This parameter defines the maximum potential above which breakdown of the material’s passivity occurs through nucleation and the stable growth of one or more corrosion pits. This is characterized by a marked and irreversible increase of the corrosion current density until it reaches the reversal current, where the potential sweep is reversed. Another feature of the F 138 steel’s polarization curve that characterizes the occurrence of pitting corrosion is the development of a hysteresis during the reversed scan (Rondelli, Vicentini, Cigada, 1997).

The region of hysteresis is characterized by the growth of pits nucleated at the critical pitting potential which are unable to repassivate immediately after the reversal in the scan direction, even at potential values lower than Ec. When the current density becomes equal to the passive current and the hysteresis closes, the protection potential (Ec) is defined, below which the existing pits are repassivated (Cahoon, Bandyopadhya, Tennesse, 1975).

The ISO 5832-9 steel displayed an electrochemical behavior rather different. The critical pitting potential for this material was not reached up to the value of potential corresponding to its transpassivity, unlike determined by Pan and coworkers (2000), who indicated a value of Ec of 1100 mV (SCE) for a high-N steel (according to ISO 5832-9 standard) tested in a similar aqueous solution. The absence of hysteresis in the polarization curve of this steel (Figure 1) indicates the absence of pitting corrosion. According to Bandy and Cahoon (1977), the increase in current density observed above approximately 1000 mV SCE can be a result of water decomposition at oxygen evolution potential, according to reaction (1) or even of uniform corrosion in the transpassive region. However, it is evident that the ISO 5832-9 steel has a much higher pitting corrosion resistance than the F 138 steel, translated by its higher value of the Ec (> 1000 mV SCE). The more positive value of Ec is attributed mainly to the presence of nitrogen in solid solution in this steel (Sivakumar, Kamachi Mudali, Rajeswari, 1994; Levey and Van Bennekem, 1995; Rondelli, Vicentini, Cigada, 1995; Azuma, Miyuki, Kudo, 1996; Grabke, ..
at Ec, the maximum current density hand, if various pits are nucleated potential sweep is reversed. That is repassivating immediately after the aggressive conditions are therefore undoubtedly will lead to the desorption of the CI ions, since segregated nitrogen cannot rapidly move away. Thus, the repulsion of the aggressive ions may be responsible for the rapid repassivation of nucleated pits in a broad interval of potentials, in steels containing a fairly high concentration of nitrogen in solution. According to the same author, rapid repassivation may be favored by the effect of nitrogen in buffering pH by the ammonium ions formation, according to reaction (2). In addition, some authors suggest the formation of corrosion resistant Cr- or Mo-nitrides in the pit bottom, suppressing the growth of the pit (Levey and Van Bennekom, 1995; Jargelius-Pettersson, 1996; Lu, Ives, Clayton, 1993).

$$N^+ + 4H^+ \rightarrow NH_4^+ \quad (2)$$

An interesting aspect of the electrochemical behavior of ISO 5832-9 steel was observed when the potential scan was reversed. In this region, it was expected that the forward and reverse potential scans would be identical, which was not the case. This behavior was expected because the breakdown of the passive film was not reached, so no stable pits, which would have led to the formation of hysteresis, developed on the metal surface. Two explanations can be proposed for this behavior. During the corrosion process in the passive or even transpassive region, the material may develop a more effective kinetic barrier against corrosion processes, for example, by the negatively charged N\(^+\) enrichment beneath the passive film or even by the thickening of the passive layer with increasingly applied potential (Grabke, 1996). Thus, when the potential scan is reversed, the kinetic barrier is greater because it was developed at nobler potentials. Having stated this, it is coherent to expect that the corrosion current density developed during the reverse scan is lower than that developed during the forward scan. A second alternative to explain the displacement of the reverse scan curve to lower current density values is attributed to the development of O\(_2\) microbubbles formed at potentials above the oxygen evolution potential, according to reaction (1). These O\(_2\) microbubbles, trapped at the metal surface, reduce the metal/solution contact area. Hence, the displacement of the reverse scan curve occurs through the reduction of the area of metal exposed to corrosion.

Another interesting behavior that stands out for its relevance is the difference in passive current density developed by the two materials. Figure 1 clearly shows that the current density developed by the ISO 5832-9 steel in the...
passive region is considerably lower than that of the F 138 steel. Passive current density is an indicative of the stability of the passive film (Levey and Van Bennekom, 1995). The lower the passive current, the more effective is the passive film as a kinetic barrier against corrosion reactions, and the lower will be the corrosion rate of the metal in the passive condition. The higher concentration of molybdenum or even the synergistic effect of nitrogen and molybdenum (Levey and Van Bennekom, 1995; Jargelius-Pettersson, 1999; Bandy and Cahoon, 1977; Lu, Ives, Clayton, 1993) through the co-segregation and the formation of a surface array which suppresses dissolution could be responsible for a passive film that is more efficient as a kinetic barrier in the ISO 5832-9 steel. The reduction in the passive current density can be attributed to the mechanism of nitrogen negatively-charged enrichment beneath the passive film. Nitrogen present in this form suppresses the adsorption of aggressive Cl\(^{-}\) ions, helping to maintain the stability and integrity of the passive film and ensuring its efficiency as a kinetic barrier against corrosive processes.

In metallic biomaterials, whose functionalities are performed inside the human body in contact with bodily fluids, the reduction in passive current density is especially relevant. A decrease in the corrosion rate inside the human body will obviously reduce the release of metallic ions into the adjacent tissues or even into the bloodstream. This release of metallic ions, chiefly chromium and nickel, is usually responsible for a large part of the adverse reactions involved in metallic implants, and may often lead to the need for their replacement (Sivakumar, Kamachi Mudali, Rajeswari, 1994; Rondelli, Vicentini, Cigada, 1997; Cahoon, Bandopadhy, Tenne, 1975).

In addition to the toxic effect associated with the release of metallic ions, it is known that the accumulation of these cations inside a crevice, i.e., an occluded cell with stagnant electrolyte, causes the concentration of aggressive ions (e.g., Cl\(^{-}\)) to increase through electrostatic attraction. The hydrolysis of metallic salts, for example according to reaction (3), also reduces the pH inside the crevice. The combination of a high concentration of Cl\(^{-}\) and high acidity severely increases the aggressiveness of the environment and stimulates the dissolution of more metallic ions inside the crevice, rendering the process self-catalytic. Therefore, the lower passive current density of ISO 5832-9 steel in comparison with that of F 138 steel suggests that crevice corrosion can be minimized by reducing the aggressiveness inside crevices, which are common in multi-component orthopedic implants. One of the most common examples of crevice is the regions that are established between the holes in a straight plate for osteosynthesis and the heads of cortical screws. Thus, there is an evident need to keep the release of ions in metallic biomaterials as low as possible.

\[
\text{M}^{+} + \text{H}_2\text{O} \rightarrow \text{MOH} + \text{H}^+ \text{Cl}^{-} \quad (3)
\]

In view of the above described observations, it was possible to verify the superiority of the ISO 5832-9 steel in terms of localized corrosion resistance when compared to the F 138 steel. The influence of nitrogen on corrosion resistance appears to be closely connected with the stability of the passive layer. This finding is confirmed by the increase in the \(E_c\) value and by the reduction in the passive current density.

The potentiostatic scratch test confirmed the superiority of the ISO 5832-9 steel when compared to the F 138, and also confirmed the high ability of the ISO 5832-9 steel to repassivate. According to the idealizers of this test method (Pessall and Liu, 1971), the potentiostatic scratch test allows the determination of the \(E_c\) value for the stainless steels in aqueous medium from the tendency of the material to repassivate and not from the tendency of the material to maintain its passivity, as in the cyclic polarization test. Thus, the \(E_c\) value, determined by this technique depends only on the metal composition and structure and not on the electrolyte characteristics, eliminating variables such as potential scan rate and specimen surface finish. In this test, after verifying the stability of the passive film for a certain period (≈ 120 s) in a given potential, where the corrosion current density must be close to zero, the mechanical damage of the passive film (scratch) is done. In this instant, the corrosion density presents a sharp increase. When repassivation occurs after the scratch, the current density must decrease rapidly to values close to zero. The applied potential is still kept during some time to verify the film stability in the repassivated region. Figure 2(a) shows this behavior for the ISO 5832-9 steel for an applied potential of 800 mV (SCE). On the other hand, when repassivation after the scratch does not occur, the current density does not stabilize in values close to zero and increases with time, as shown in Figure 2(b) for the F 138 steel for an applied potential of 400 mV (SCE). Then the \(E_c\) value is defined as the potential above which the repassivation of the damaged surface by the scratch no longer occurs. In this test, the F 138 steel presented an average \(E_c\) value of 427 ± 34 mV (SCE). The ISO 5832-9 steel, on the other hand, showed a much larger repassivation tendency with an \(E_c\) value above 800 mV (SCE), which was the upper limit for this test.

The increase of the \(E_c\) value for this test may also be attributed to the nitrogen in solid solution in the ISO 5832-9 steel. Resorting once more to the mechanism proposed by Grabke (1996), immediately after the breakdown of the passive film (mechanically in this case), there is a segregation of nitrogen, negatively charged (N\(^{\text{V}}\)), on the metal surface, by anodic dissolution of the unprotected surface. This segregation promotes the removal of aggressive ions (Cl\(^{-}\)) by the repulsive interaction with the segregate species N\(^{\text{V}}\). A sufficiently adequate condition is created so that repassivation occurs, even in potentials as noble as +800 mV (SCE).
Figures 3 and 4 illustrate the results of the SEM examinations aimed at characterizing the relevant features of corrosive attack on the surfaces of the two steels submitted to the cyclic potentiodynamic polarization test. These examinations revealed the presence of pits that steadily grew, i.e., lacerlike pits (Figure 3(a)), on the surface of the F 138 steel specimens and, on the other hand, the absence of these pits on the surface of the ISO 5832-9 steel. This finding corroborates the already formulated assumptions based on the cyclic polarization behavior, and contributes to the statement that the presence of hysteresis in the cyclic polarization curve confirms the occurrence of pitting corrosion, while the absence of hysteresis excludes the possibility of this type of corrosion. Lacerlike pits are responsible for the development of hysteresis in the cyclic polarization curve of the F 138 steel. The dimension of these pits favors the establishment of occluded cells and, consequently, the development of an extremely aggressive environment inside them.

The SEM examination of the F 138 steel specimens also revealed the following characteristics: (1) no evidences of corrosion associated with non-metallic inclusions was found; (2) a large number of small pits were observed in an incipient stage of growth, or even pits that had firstly initiated but repassivated, which could be responsible for the serrated portion in the passive region of the polarization curve (Figure 1); (3) the incipient pits remained approximately equi-axial, bordered by facets (Figure 3(b)). According to Newman and Franz (Newman and Franz, 1984), crystallographic facets are formed in the initial stage of growth, when the concentration of chloride ions inside the pit is still low compared to the concentration inside a pit in an advanced stage of growth. During growth, coalescence of existing pits with newly nucleated ones surrounding them may occur. When the conditions inside the pit become sufficiently aggressive, an active dissolution process is initiated, preferentially at the pit bottom, giving rise to deeper, irregular pits, as shown in Figure 3(a).

In the case of the ISO 5832-9 steel, corrosion pitting in an advanced stage of growth was not observed. However, a selective attack associated to the Z-phase precipitates (CrNbN) - abundant on the microstructure of this type of steel (Giordani et al., 2004) - has been observed, as shown in Figure 4. The selective attack removed most of the smaller particles, indicating that Z-phase, or even its surroundings, is less noble than the remaining austenitic matrix and actively dissolves at high potentials. If the Z-phase precipitation site dissolution is an anodic process, it may contribute to the increased current density in the high potential region (Figure 1). Since smaller Z-phase particles can be removed from the exposed surface, the shifting of the curve during reverse scan to lower current density values can also be attributed to the reduction of actively corrosive sites.

Only after the potentiodynamic polarization test, at potentials above 800 mV SCE, was the degradation of coarse primary Z-phases by cracking (Figure 4(b)) observed, which was not investigated in this study. This degradation could be related to some mechanism of hydrogen embrittlement or even the formation of some compounds inside the Z-phase particle.

The addition of Nb and its fine precipitation at Z-phase, during controlled thermomechanical processing, promotes grain refinement of the ISO 5832-9 steel (Giordani, Jorge Jr., Balancin, 2005). The association of fine grain structure with some amount of nitrogen in solid solution is responsible for the high strength of this austenitic stainless steel, even in the annealed condition. On the other hand, the coarse
Enrico J. Giordano et al.

Figure 3 - SEM examination on the surface of the specimens of F 138 steel subjected to potentiodynamic cyclic polarization test: (a) lacelike pit in advanced stable growth; (b) crystallographic (faceted) pits in an incipient stage of growth or even pits that initiated but repassivated

Figure 4 - SEM examination on the surface of specimens of ISO 5832-9 steel subjected to potentiodynamic cyclic polarization tests: selective attack of the Z-phase precipitates.

primary Z-phase precipitates, besides acting as fatigue crack initiation sites (Giordani et al., 2004), involve the removal of nitrogen, which is mainly responsible for the highly localized corrosion resistance of this steel, out of the solid solution. Based on this finding, one can suggest that the Nb addition should be carefully controlled so that coarse and excessive primary Z-phase precipitation is avoided.

4. Conclusions

Potentiodynamic and potentiostatic polarization tests in 0.9% NaCl solution revealed that the ISO 5832-9 steel has a far higher pitting corrosion resistance than the F 138 steel. This property is attributed mainly to the increased passive film stability and high ability to repassivate, favored by the presence of nitrogen in interstitial solid solution in the austenite of this steel. SEM examination confirmed the presence of steadily growing corrosion pits (lacelike pits) on the surface of F 138 steel and the absence of such pits in the specimens of the ISO 5832-9 steel.

Potentiodynamic polarization test also show, at high potentials, that a selective attack associated to the Z-phase (CrNbN) precipitation sites - abundant on the microstructure of the ISO 5832-9 steel - removed most of the smaller particles, indicating that these sites are less noble than the remaining austenitic matrix, and degraded the larger ones.

5. Acknowledgements

The authors are indebted to CNPq and FAPESP for their financial support of this work.
6. References
AZUMA S., MIYUKI H., KUDO T. Effect of alloying nitrogen on crevice corrosion of austenitic stainless steels. ISIJ International, v. 36, n. 7, p. 793-798, 1996.
BANDY R., CAHOON J.R. Effect of composition on the electrochemical behaviour of austenitic stainless steel in Ringer’s solution. Corrosion, v. 33, n. 6, p. 204-208, 1977.
CAHOON J.R., BANDYOPADHYA R., TENNESE E. The concept of protection potential applied to the corrosion of metallic orthopedic implants. Journal of Biomedical Materials Research, v. 9, p. 259-264, 1975.
GIORDAN E.J., GUIMARAES V.A., PINTO T.B., FERREIRA I. Effect of precipitates on the corrosion-fatigue crack initiation of ISO 5832-9 Stainless Steel Biomaterials. International Journal of Fatigue, v. 26, p. 1129-1136, 2004.
GIORDAN E.J., JORGE Jr. A.M., BALANCIN O. Evidence of strain-induced precipitation on a Nb- and N-bearing austenitic stainless steel biomaterial. Materials Science Forum, v. 500-501, p. 179-186, 2005.
GIORDAN E.J., FERREIRA I., BALANCIN O. Propriedades mecânicas e de corrosão de dois aços inoxidáveis austeníticos utilizados na fabricação de implantes ortopédicos. REM - Revista da Escola de Minas, v. 60, n. 1, p. 55-62, 2007.
GRABKE H.J. The role of nitrogen in the corrosion of iron and steels, ISIJ International, v. 36, n. 7, p. 777-786, 1996.
JARGELIUS-PETTERSSON R.F.A. Electrochemical investigation of the influence of nitrogen alloying on pitting corrosion of austenitic stainless steels. Corrosion Science, v. 41, p. 1639-1664, 1999.
JARGELIUS-PETTERSSON R.F.A. Sensitization behaviour and corrosion resistance of austenitic stainless alloyed with nitrogen and manganese. ISIJ International, v. 36, n. 7, p. 818-824, 1996.
KAMACHI MUDALI U., DAYAL R.K., GNANAMOORTHY J.B., RODRIGUEZ P. Relationship between pitting and intergranular corrosion of nitrogen-bearing austenitic stainless steels. ISIJ International, v. 36, n. 7, p. 799-806, 1996.
LEVEY P.R., VAN BENNEKOM A. A Mechanistic study of the effects of nitrogen on the corrosion properties on stainless steels. Corrosion, v. 51, n. 12, p. 911-921, 1995.
LIM Y.S., KIM J.S., Kwon H.S., KATADA Y. The influence of microstructure and nitrogen alloying on pitting corrosion of type 316 L and 20 wt.% Mn-substituted type 316 L stainless steel. Corrosion Science, v. 43, p. 53-68, 2001.
LU Y.C., IVES M.B., CLAYTON C.R. Synergism of alloying elements and pitting corrosion resistance of stainless steels. Corrosion Science, v. 35, n. 1-4, p. 89-96, 1993.
NEWMAN R.C., FRANZ E.M. Growth and repassivation of single corrosion pits in stainless steel. Corrosion, v. 40, p. 325-330, 1984.
PAN J., KARLEN C., ULFVIN C. Electrochemical study of resistance to localized corrosion of stainless steel for biomaterial applications. Journal of the Electrochemical Society, v. 147, p. 1021-1025, 2000.
PESSLN N., LIU C. Determination of critical pitting potentials of stainless steels in aqueous chloride environments. Electrochimica Acta, v. 16, p. 987-1003, 1971.
PICKERING F.B. Lille, France, 1988. Some beneficial effect of nitrogen in steels. In: INTERNATIONAL CONFERENCE ON NITROGEN STEELS, Proceedings ed. by Foc, J. & Hendry, A. The Institute of Metals, London, 1989, p.10-31.
RONDELLI G., VICENTINI B., CIGADA A. Influence of nitrogen and manganese on localized corrosion behaviour of stainless steels in chloride environments. Materials and Corrosion, v. 46, n. 6, p. 628-632, 1995.
RONDELLI G., VICENTINI B., CIGADA A. Localized corrosion tests on austenitic stainless steels for biomedical applications. British Corrosion Journal, v. 32, n. 3, p. 193-196, 1997.
SIVAKUMAR M., KAMACHI MUDALI U., RAJESWARI S. In vitro electrochemical investigations of advanced stainless steels for applications as orthopaedic implants. Journal of Materials Engineering and Performance, v. 3, n. 6, p. 744-753, 1994.
TRUMAN J.E., COLEMAN M.J., PIRT K.R. Note on the influence of nitrogen content on the resistance to pitting corrosion of stainless steels. British Corrosion Journal, v. 12, n. 4, p. 236-238, 1977.
WILDE B.E., WILLIAMS E. Use of current/voltage curve for study of localized corrosion and passivity breakdown on stainless steels in chloride media. Electrochimica Acta, v. 16, p. 1971-&, 1971.
Artigo recebido em 03/06/2009 e aprovado em 18/01/2010.

Electrochemical behavior of two austenitic stainless steel biomaterials