OpenMPIData: An initiative for freely accessible magnetic particle imaging data

Tobias Knopp a, b, *, Patryk Szwargulski a, b, Florian Griese a, b, Matthias Gräser a, b

a Section for Biomedical Imaging, University Medical Center Hamburg-Eppendorf, Germany
b Institute for Biomedical Imaging, Hamburg University of Technology, Germany

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ABSTRACT

Magnetic particle imaging is a tomographic imaging technique capable of measuring the local concentration of magnetic nanoparticles that can be used as tracers in biomedical applications. Since MPI is still at a very early stage of development, there are only a few MPI systems worldwide that are primarily operated by technical research groups that develop the systems themselves. It is therefore difficult for researchers without direct access to an MPI system to obtain experimental MPI data. The purpose of the OpenMPIData initiative is to make experimental MPI data freely accessible via a web platform. Measurements are performed with multiple phantoms and different image sequences from 1D to 3D. The datasets are stored in the magnetic particle image data format (MDF), an open document standard for storing MPI data. The open data is mainly intended for mathematicians and algorithm developers working on new reconstruction algorithms. Each dataset is designed to pose a specific challenge to image reconstruction. In addition to the measurement data, computer aided design (CAD) drawings of the phantoms are also provided so that the exact dimensions of the particle concentrations are known. Thus, the phantoms can be reproduced by other research groups using additive manufacturing. These reproduced phantoms can be used to compare different MPI systems.

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* Corresponding author. Section for Biomedical Imaging, University Medical Center Hamburg-Eppendorf, Germany.
E-mail address: t.knopp@uke.de (T. Knopp).

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In the following subsections we outline the phantoms and parameters that were used to acquire the magnetic particle imaging (MPI) datasets. All measurements were performed using the preclinical MPI scanner shown in Fig. 1. In all descriptions we refer to the coordinate system shown in the figure.
1.1. Phantoms

The measurements were performed with three different object phantoms. In all cases the tracer perimag (micromod, Rostock) was used for contrast generation. Pictures of the three phantoms are shown in Fig. 2.

The first phantom is a cone having a tip radius of 1 mm, an apex angle of $10^\circ$ and a height of 22 mm. The total volume of the cone is 683.9 μL. The tracer concentration used in the experiments was 50 mmol(Fe)/L. The phantom can be rendered in 3D resembling the cone or can be cut in a layer view to see either a circle (yz plane) or a triangle with flattened tip (xz or xy plane).

The resolution phantom consists of five tubes with 1 mm radius filled with perimag of concentration 50 mmol(Fe)/L. The five tubes have a common origin in one point of the phantom. From that point they run in different directions in the xy and yz plane. While one tube points directly in y direction, the two tubes in the yz plane have an angle of $10^\circ$ and $15^\circ$ to the y axis. The two tubes in the xy plane have an angle of $20^\circ$ and $30^\circ$ to the y axis. The higher angles in the yz plane are due to the stronger gradient strength of the selection field in z direction, which results in higher spatial resolution. In order to determine the resolution of the reconstructed particle concentration one can consider xz planes and test if the tubes can be resolved. By varying the distance of the chosen plane to the origin of the tubes, the tube distance can be varied.

The last phantom is a concentration phantom consists of 8 cubes with 2 mm edge length and 8 μL volume. The cubes are placed at the corners of a cuboid with 12 mm distance in the x and y directions and 6 mm distance in the z direction. The cubes are numbered from 1 to 8 starting with the top layer on the front left (positive x and y directions), counting clockwise. Then starting with the lower layer with number 5 on the front left (positive x and y directions), counting clockwise. The numbers are also indicated in the CAD sketch in Fig. 2. The 8 cubes are filled with different concentrations starting from 100 mmol(Fe)/L and reducing the concentration by a factor of 1.5 from one to another cube. The concrete concentrations are listed in the following table. They are arranged in a way that the highest and the lowest concentration are not within the same plane.

| Number | 1      | 2      | 3      | 4      | 5      | 6      | 7      | 8      |
|--------|--------|--------|--------|--------|--------|--------|--------|--------|
| Concentration [mmol(Fe)/L] | 44.4   | 100    | 29.6   | 8.77   | 19.7   | 66.6   | 13.1   | 5.85   |
1.2. Sequences

Each phantom was measured with three different measurement sequences [3]. All three are 3D sequences, but the number of applied excitation directions is increased from one to three. In case of the 1D and 2D excitation, the dimension with no excitation is sampled by moving the phantom stepwise using a robot. For the 1D excitation this movement was first performed in the $z$ direction and then in the $y$ direction, i.e. $xz$ slices were measured slice by slice. The following table summarizes the parameters of the three measurement sequences.

![Resolution Phantom](image1.png)
![Shape Phantom](image2.png)
![Dilution Phantom](image3.png)

Fig. 2. Phantoms used in the open MPI datasets.
1.3. Phantom datasets

For each phantom and for each sequence a measurement was performed. The measurements are listed in the following table. The study name and the experiment number can uniquely identify them.

| Parameter                          | 1D Cartesian | 2D Lissajous | 3D Lissajous |
|------------------------------------|--------------|--------------|--------------|
| Drive-Field Amplitude              | $12 \text{ mT} \times 0 \text{ mT} \times 0 \text{ mT}$ | $12 \text{ mT} \times 12 \text{ mT} \times 0 \text{ mT}$ | $12 \text{ mT} \times 12 \text{ mT} \times 12 \text{ mT}$ |
| Drive-Field Frequency              | $2.5/102 \text{ MHz} \times 2.5/96 \text{ MHz} \times 2.5/99 \text{ MHz}$ | | |
| Selection-Field Gradient           | $-1.0 \text{ T/m} \times -1.0 \text{ T/m} \times 2.0 \text{ T/m}$ | | |
| Repetition Time                    | $40.8 \mu s$ | $652.8 \mu s$ | $21.54 \text{ ms}$ |
| Number of Patches                  | $1 \times 19 \times 19$ | $1 \times 1 \times 19$ | $1 \times 1 \times 1$ |
| Number of Periods per Patches      | 1000         | 1000         | 1            |
| Number of Frames                   | 1            | 1            | 1000         |

1.4. Calibration datasets

In addition to the object measurements that contain the data of the right hand side of the MPI imaging equation $\mathbf{S} \mathbf{c} = \mathbf{u}$, OpenMPIData contains for each measurement sequence two calibration measurements that basically store the system matrix $\mathbf{S}$. All calibration scans are measured using a voxel-shaped delta sample of size $2 \text{ mm} \times 2 \text{ mm} \times 1 \text{ mm}$ filled with perimag (concentration $100 \text{ mmol(Fe)/L}$). The delta sample is moved on a regular grid covering a volume of size $24 \text{ mm} \times 24 \text{ mm} \times 12 \text{ mm}$. While the first calibration scan is measured at $19 \times 19 \times 19$ grid positions, the second calibration scan is measured at $37 \times 37 \times 37$ grid positions.

### Study summary

| Study                  | Experiment Number | Grid           | Scanner | Sequence   | Tracer |
|------------------------|-------------------|----------------|---------|------------|--------|
| shapePhantom           | 1                 | $19 \times 19 \times 19$ | Bruker  | 1D Cartesian | perimag |
| shapePhantom           | 2                 | $19 \times 19 \times 19$ | Bruker  | 2D Lissajous | perimag |
| resolutionPhantom      | 3                 | $19 \times 19 \times 19$ | Bruker  | 3D Lissajous | perimag |
| resolutionPhantom      | 1                 | $19 \times 19 \times 19$ | Bruker  | 1D Cartesian | perimag |
| concentrationPhantom   | 2                 | $19 \times 19 \times 19$ | Bruker  | 2D Lissajous | perimag |
| concentrationPhantom   | 3                 | $19 \times 19 \times 19$ | Bruker  | 3D Lissajous | perimag |

### Experimental design, materials, and methods

The OpenMPIData project has two different purposes. The first aim is to provide a fixed number of reference datasets that cover several challenging aspects for image reconstruction methods. These datasets are content of the present document and documented in detail. The second aim of the OpenMPIData project is to provide a platform where open MPI data can be hosted. In order to add new datasets to the platform one can create an issue at the Github project page.
The measurements discussed in this paper were measured in February 2018 using the preclinical MPI scanner (Bruker, Ettlingen) that was installed at the University Medical Center Hamburg-Eppendorf in 2014. All measurements were done with the equipped receive coils. The phantoms were designed with the CAD software SolidWorks and printed with a stereolithography 3D printer (Form2, Formlabs). The phantoms were then filled with perimag that was first diluted to the concentration given in the data section. The phantoms were mounted at a rod provided by the vendor of the MPI system and moved into the scanner center using a robot. Then, the measurements were performed using the system software ParaVision. Calibration measurements were done using the calibration method within the system software ParaVision. Instead of a phantom, the delta sample was mounted onto the rod that moves the sample into the scanner bore.

After performing the measurements, all measurements were converted from the proprietary vendor data format into the open Magnetic Particle Imaging Data Format (MDF) [4] using the software package MPIFiles.jl [5]. The OpenMPIData Github repository contains example scripts that perform a baseline reconstruction and visualize the results. The baseline reconstruction is based on the software package MPIReco.jl [6]. Example reconstructions of all phantoms for the 3D Lissajous sequence are shown in Fig. 3.

**Fig. 3.** Baseline reconstruction results using the Kaczmarz algorithm for the shape phantom (top left), the resolution phantom (top right), and the concentration phantom (bottom right). In all cases the 3D Lissajous measurement was reconstructed. For the shape phantom maximum intensity projections (MIP) are shown.
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Conflict of Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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