Experimental verification of the application of lateral buildup ratio on the 4-MeV electron beam

James C.L. Chow\(^1\)\(^2\),\(^a\) and Scott Newman\(^1\)

\(\text{Medical Physics Department,} \ 1\ \text{Grand River Regional Cancer Center, Grand River Hospital,} \ \text{PO. Box 9056, 835 King Street West, Kitchener, Ontario N2G 1G3; Department of Physics,} \ 2\ \text{University of Waterloo, 200 University Avenue, Waterloo, Ontario N2L 3G1 Canada}

\text{james.chow@rmp.uhn.on.ca}

Received 17 June 2005; accepted 12 December 2005

The lateral buildup ratio (LBR) used to estimate the depth dose distribution of electron beams for an irregular cutout field was obtained for a 4-MeV energy beam from a Varian 21 EX linear accelerator. The depth-dose curves for a group of circular cutout fields starting from a 2-cm diameter were measured. Electron diodes were used in a large water tank to measure the LBR values for 6, 9, 12, and 16 MeV electron beam energies and a 10 × 10 cm\(^2\) applicator. The results agreed with the published data. When the same equipment, setup, and technique were used to determine the LBR values for the 4-MeV energy beam, the values were only reasonable, being within the clinical treatment range (i.e., LBR < 1) for the smallest 6 × 6 cm\(^2\) applicator. The calculated LBR values were clinically unacceptable for the circular cutout fields with a diameter larger than 2 cm with the 10 × 10 cm\(^2\) applicator. The difficulty in the LBR measurement may be due to the significant contribution of scattered electrons from the beam defining system. This study also focused on how well the sigma values for the 4-MeV beam can predict depth-dose curves for other field sizes and whether the values are applicator-dependent.

PACS numbers : 87.53.Fs; 87.53.Hv; 87.66.Jj

Key words: electron therapy, dosimetry, lateral buildup ratio

I. INTRODUCTION

It is well known that the elementary pencil beam algorithms\(^{1-5}\) have been used to calculate the dose distribution for electron beam treatment planning. These algorithms required measured beam data of depth doses and beam profiles which varied with the collimation systems of different accelerators. For that, the dose per monitor unit of irregularly shaped cutout fields had individually been measured in clinical practice. These patient-specific measurements were time-consuming, so different models based on the pencil beam approach were proposed to calculate the output factor in irregularly shaped electron fields.\(^{6-9}\) Khan et al.\(^{10-12}\) introduced a semi-empirical model based on the lateral spread of the pencil beam and proposed a function called the lateral buildup ratio (LBR). It is defined as the ratio of dose at a point of depth for a given circular field to the dose at the same point for a reference broad field, which is large enough to provide the lateral scatter equilibrium for the incident fluence and profile. The LBR represents the fractional change in dose at a field point due to the loss of scatter relative to the large reference field and can be calculated from the percentage depth dose (PDD) normalized near to the surface. The ratio is related to the lateral pencil beam spread function, \(\sigma(z, E)\), where \(z\) is the depth, and \(E\) is the energy of a circular electron beam of radius \(r\).\(^{11,12}\) By using the \(\sigma(z, E)\) values derived from the measured LBRs for a small circular reference field (usually with a 2-cm diameter), sector-type integration can be used to calculate the average LBR at any depth of an irregular field.\(^{10,12-14}\)

\(^a\) Permanent address: Radiation Medicine Program, Princess Margaret Hospital, 610 University Avenue, Toronto, Ontario M5G 2M9 Canada
Khan et al. have demonstrated the convenience and accuracy of using the LBR to calculate the electron beam output factors for 6, 9, 12, 16, and 20 MeV electron beams,(10–12) and Higgins et al.(15) have further evaluated the application of this model to calculate dose outside the field edge and in a heterogeneous media. Although the above five electron beam energies are more frequently used by most centers for clinical treatment, 4 MeV is an available option.(16) This energy, with its relatively shorter practical range and depth of maximum dose \(d_m\), is particularly useful for treating superficial lesions when the superficial X-ray treatment unit is not available.(17–20) However, 4-MeV beam data such as depth-dose and beam profiles are more unstable, due to difficult beam tuning, and are difficult to measure accurately compared to higher energies.(21–23) The aim of this study is to investigate whether the LBR approach is beneficial to the 4-MeV electron beam through measurements.

II. MATERIALS AND METHODS

A. Beam profiles and PDD

The beam profiles and PDD curves of the electron beams were measured using a scanning water tank system (RFA 300, Scanditronix Medical AB with Omni Pro 6 software). A waterproof high-doped p-type silicon diode (Scanditronix Medical AB, EFD-3G) was used to measure both the beam profiles and PDD at the central beam axis. The thickness of the silicon chip was 0.5 mm, and the diameter of the active area was 2 mm. Since some of the circular cutout fields were too small to put a reference detector on the beam path, the reference dose signal for the measurements was obtained from the internal monitoring ionization chamber within the gantry head. A Varian 21 EX linear accelerator with 4, 6, 9, 12, and 16 MeV clinical electron beams was used in the measurement. The 4-MeV electron beam uses a scattering foil designed for the specific energy. The central axis for the PDD curve was located according to the peak position of the profile for the measurement. This was particularly important when performing the PDD measurement for a very small circular cutout field (close to 2 cm in diameter), where the beam penumbra was relatively large for such a low energy due to electronic disequilibrium.

The diode was positioned vertically, perpendicular to the water surface. This setting made the sampling resolution dependent on the thickness of the diode sensitive volume (~0.5 mm). The position of the sensitive region from the detector front surface was provided by the manufacturer and verified in this study, and was considered the effective point of measurement. A depth ionization curve was scanned first to determine the position of \(d_m\) before the beam profile scanning. The sensitive volume of the diode was then positioned there, and the beam profiles along the in- and cross-plane directions were scanned. Both the 6 × 6 cm² and 10 × 10 cm² applicators were used in the measurement. For the 10 × 10 cm² applicator, circular cutouts with diameters of 2, 3, 4, 6, 8, and 10 cm and a square cutout of 10 × 10 cm² were made. For the 6 × 6 cm² applicator, circular cutouts with diameters 2, 2.5, 3, 4, 5, and 6 cm and a square cutout of 6 × 6 cm² were made. The thickness of cutout in this study was 15 ± 1 mm, and the field edges were sharp and not divergent. The beam profiles for all cutouts of the 10 × 10 cm² applicator with 4, 6, 9, 12, and 16 MeV were measured. For the cutouts of the 6 × 6 cm² applicator, only the 4-MeV beam profiles were measured.

The position of the surface was determined by noting the dose variation in the diode reading at the water–air interface. Percentage depth ionization (PDI) curves were measured with the highest sampling resolution and the slowest speed. Central beam axis PDI curves for the different cutouts of the 10 × 10 cm² applicator as mentioned above were measured for all five energies. For the cutouts of the 6 × 6 cm² applicator, only the 4-MeV PDI curves were measured. All measurements were taken using a source-to-surface distance (SSD) of 100 cm with an air gap of 5 cm. These measurements were carefully repeated one by one within the same day. It was found that the repeated scan agreed with the original results within ≈0.5%. The SSD and zero
water level were checked frequently in order to prevent any physical effects, such as evaporation, from introducing measurement error. In addition, the actual cutout dimensions used for the measurements were checked to ensure that the center of the circular cutout was positioned at the central beam axis within ±2 mm. The radiation characteristics of the diode were verified with the ionization chamber to confirm that the depth ionization curve obtained by the diode could be used as the depth-dose curve without correction.

B. Formalism and LBR calculation

The LBR is defined as

\[ LBR(r, z, E) = \frac{D(r, z, E)}{D(r_{\infty}, z, E)} \cdot \frac{\Phi(r_{\infty}, E)}{\Phi(r, E)}, \]  

where \( D \) is the dose, \( r \) is the radius of the field defined at the water surface (in our study, it was SSD = 100 cm), \( z \) is the depth, and \( E \) is the incident electron beam energy. \( \Phi \) is the incident fluence, and \( r_{\infty} \) is the broad field radius, that is, the radius of field large enough to provide lateral scatter equilibrium. In this study, the variation of the incident fluence factor in Eq. (1) was factored out by normalizing the depth-dose data of the circular field to the dose near to the surface. The broad fields for the 6 × 6 cm\(^2\) and 10 × 10 cm\(^2\) applicator were selected to be the open square cutout fields of 6 × 6 cm\(^2\) and 10 × 10 cm\(^2\), respectively.

Since LBR can be written as

\[ LBR(R, z) = 1 - \exp\left(-\frac{R^2}{\sigma_r(z)}\right), \]  

and therefore

\[ \sigma_r(z) = \frac{R}{\ln\left(\frac{1}{1 - LBR(R, z)}\right)}, \]  

provided that the LBR value is smaller than one, it is also possible to determine the \( \sigma_r(z) \) values with respect to the depth, \( z \), or normalized depth, \( z/R_p \), for each electron beam energy.

III. RESULTS

Figure 1 is a plot of \( \sigma_r \) as a function of the normalized depth for the 4, 6, 9, 12, and 16 MeV energies. The values were calculated using the LBR data for the 2-cm diameter circular cutout as suggested by Khan et al.\(^\text{(10)}\). According to the ICRU Report 35 (ICRU 1984),\(^\text{(24)}\), measuring the dose at a depth of 0.5 mm instead of at the surface was suggested as a normalization to ensure proper detector positioning and to avoid measurements in the unstable buildup region near the surface. Figures 2(a) and 2(b) show the 4-MeV PDD curves using the circular cutouts with 2, 2.5, 3, 4, 5, and 6 cm diameters for the 6 × 6 cm\(^2\) and 10 × 10 cm\(^2\) applicators, respectively. The PDD curves were normalized to their doses at 0.5 mm from the water surface. The LBR curves against the normalized depth, \( z/R_p \), calculated from Figs. 2(a) and 2(b), are shown in Figs. 3(a) and 3(b), respectively. All LBR values larger than one were eliminated in Fig. 3.
Fig. 1. $\sigma_r$ plotted against the normalized depth, $z/R_p$, for the 4 to 16 MeV electron beam. The values were calculated from the LBR data for the 2-cm diameter field for the $10 \times 10$ cm$^2$ applicator.

Fig. 2. 4 MeV PDD curves of circular cutouts with diameters 2, 2.5, 3, 4, 5, and 6 cm for the (a) $6 \times 6$ cm$^2$ applicator and the (b) $10 \times 10$ cm$^2$ applicator. All curves are normalized to the dose near the water surface (0.5 mm depth of water).
IV. DISCUSSION

In Fig. 1, the \( \sigma \) values were calculated using the 2-cm diameter cutout for the 10 \( \times \) 10 cm\(^2\) applicator. These values were verified and agree with the similar published results\(^{10}\) except for the 4-MeV energy. It was found that, as previously reported,\(^{12}\) the PDD calculated using our \( \sigma \) values can reproduce the PDD for other field sizes with energies from 6 to 16 MeV within \( \pm 1\% \) error bar, while for the 4-MeV, the error in reproducing the PDD is \( \pm 4\% \). Moreover, the \( \sigma \) versus \( z/R_p \) and LBR versus \( z/R_p \) are independent of the cutout shape as reported.\(^{10}\) There is no problem in the application of LBR in the above energy range.

In Fig. 2(a), showing the PDD curves of the 6 \( \times \) 6 cm\(^2\) applicator, it was found that beyond 1.5 cm, the depth doses of the circular cutouts with diameters \( \geq 5 \) cm are very close or even very slightly larger (about 3% on average) than that of the broad field. Such uncertainty is larger than the reproducibility error bar of the measurement (\( \pm 0.5\% \)). In Fig. 2(b), there was a more significant increase in the depth doses of cutouts (\( \geq 5 \) cm) than in the broad field, in the bremsstrahlung tail range for the 10 \( \times \) 10 cm\(^2\) applicator. In the two figures, when the electronic equilibrium condition had been reached for those sufficiently large circular fields (i.e., \( \geq 5 \) cm diameter), measurement uncertainty of the depth dose near to the bremsstrahlung tail...
became significant in the LBR calculation. Or it is understood that those large circular fields can also be recognized as broad fields. For the 4-MeV energy, neglecting the consideration for the physical effects from the measurement, the PDD curve is very difficult to predict through measurements, especially for depths larger than 2 cm because the scattered electrons from the applicator and cutout contribute significantly to the doses, due to its relatively large electron angular scattering cross section. Such dose contribution from the scattered electrons is difficult to predict because it depends on the material and geometry of the beam defining system. The scattered electrons from the applicator have a different energy spectrum and angular scattering cross section than the primary incident electrons. The difference of field size dependence between the $6 \times 6$ cm$^2$ and $10 \times 10$ cm$^2$ applicator is also probably due to the different beam defining system used, although both applicators have the same photon jaws setting ($20 \times 20$ cm$^2$). For highly accurate results, Monte Carlo investigations would be useful but are beyond the scope of this study.

Figure 3 shows the LBR values calculated from Fig. 2. In Fig. 3(a), the LBR values are seen to be nonsense beyond 15 mm or normalized depth ($z/R_p$) of 0.88. However, the values are reasonable if the focus is restricted to the clinical treatment range between 7 mm ($d_{m}$) and 14 mm (i.e., 100 to 50% isodose contour), or normalized depth between 0.41 and 0.82, and excludes the LBR calculated from the large circular cutouts equivalent to the broad field. The discontinuities near $R_p$ in Fig. 3(a) are due to the measured depth-dose uncertainty as explained in Fig. 2(a). However, in Fig. 3(b) for the $10 \times 10$ cm$^2$ applicator, it is seen that only the LBR values of circular cutouts with 2 cm and 3 cm diameter are reasonable. It seems that the LBR was difficult to measure and calculate for the 4-MeV electron energy, using an applicator larger than $6 \times 6$ cm$^2$ within the clinical treatment range. In the discontinuity range of the figures, the sigma values calculated using the PDD data of the 2-cm cutout could not accurately predict the PDD data for other field sizes. This is different for higher energies from 6 to 16 MeV, where the PDD calculated using sigma values for a 2-cm diameter cutout could reproduce the PDD for other field sizes as reported.$^{(10)}$ Since the PDD data for higher energies is applicator-independent, according to our measurement, the sigma values and LBR versus $z/R_p$ are also applicator-independent; this has been verified for the 6-MeV electron beam. However, this is not the case for the low-energy 4-MeV beam, as shown in Figs. 2 and 3. Different LBR versus $z/R_p$ should be plotted for different applicators.

V. CONCLUSION

The LBR values of the 4-MeV electron energy using the Varian 21 EX accelerator were measured and calculated. It was found that, for a small applicator size of $6 \times 6$ cm$^2$, the calculated LBR values were reasonable and within the clinical treatment range. However, when a larger $10 \times 10$ cm$^2$ applicator was used, the LBR values with circular fields larger than 2 cm in diameter were not reasonable compared to those of higher energies. This is because the PDD for a range of cutouts was higher than the $10 \times 10$ cm$^2$ applicator broad beam PDD at certain depth ranges, and the LBR model breaks down under these conditions. It was found that the depth-dose uncertainty increased when an insert and applicator larger than $6 \times 6$ cm$^2$ was used. Another reason is that the lateral scatter/electronic equilibrium is more easily reached by increasing the circular cutout size from 2 cm diameter compared to higher energies. Since, in the output (dose per monitor unit), calculation of an irregular field requires sector-type integration of LBR with a variation of radii data, the uncertain LBR values in the larger circular fields cause significant error in the output estimation of the 4-MeV electron beam compared to those at higher energies. Based on the measured results in this study, it can be concluded that the LBR could not be used to model the 4-MeV electron beam well.
REFERENCES

1. Perry DJ, Holt JG. A model for calculating the effects of small inhomogeneities on electron beam dose distribution. Med Phys. 1980;7:207–215.

2. Brahme A, Lax I, Andreo P. Electron beam dose planning using discrete Gaussian beams, mathematical background. Acta Radiol Oncol. 1981;20:147–158.

3. Hogstrom KR, Mills MD, Almond PR. Electron beam dose calculations. Phys Med Biol. 1981;26:445–459.

4. Werner BL, Khan FM, Deibel FC. A model for calculating electron beam scattering in treatment planning. Med Phys. 1982;9:180–187.

5. Jette D. The application of multiple scattering theory to therapeutic electron dosimetry. Med Phys. 1983;10:141–146.

6. Dutreix A, Briot E. The development of a pencil-beam algorithm for clinical use at the Institut Gustave Roussy. In: Nahum AE, editor. The computation of dose distributions in electron beams, radiotherapy. Sweden: University of Umea; 1990: 242–270.

7. Mills MD, Hogstrom KR, Almond PR. Prediction of electron beam output factors. Med Phys. 1982;9:60–68.

8. Bruvinvis IAD, Amstel AV, Eleveit AJ, Van der Laarse R. Dose calculation for arbitrarily shaped electron fields. Acta Radiol Suppl. 1983;364:73–79.

9. McParland BJ. A method of calculating the output factors of arbitrarily shaped electron fields. Med Phys. 1989;16:88–93.

10. Khan FM, Higgins PD, Gerbi BJ, Deibel FC, Sethi A, Mihailidis DN. Calculation of depth dose and dose per monitor unit for irregularly shaped electron field. Phys Med Biol. 1998;43:2741–2754.

11. Khan FM, Higgins PD. Calculation of depth dose and dose per monitor unit for irregularly shaped electron fields: An addendum. Phys Med Biol. 1999;44:N77–N80.

12. Khan FM, Higgins PD. Field equivalence for clinical electron beams. Phys Med Biol. 2001;46:N9–N14.

13. Jones D, Andre P, Washington JT, Hafermann HD. A method for the assessment of the output of irregularly shaped electron fields. Br J Radiol. 1990;63:59–64.

14. Wu RK, Wang W, El-Mahdli AM. Irregular field output factors for electron beams. In: Bruvinvis IAD, van der Giessen PH, van Kleffens HJ, and Wittkamper FW, editors. Proceedings of the 9th international conference on the use of computers in radiation therapy. Sweden: Scheveningen; 1987: 453–456.

15. Higgins PD, Gerbi PD, Khan FM. Application of measured pencil beam parameters for electron beam model evaluation. Med Phys. 2003;30:514–520.

16. Followill DS, Davis DS, Ibbott GS. Comparison of electron beam characteristic from multiple accelerators. Int J Radiat Oncol Biol Phys. 2004;59:905–910.

17. Walker C, Wadd NJ, Luraft HH. Novel solutions to the problems encountered in electron irradiation to the surface of the head. Br J Radiol. 1999;72:787–791.

18. Scholten AN, Griep C, Davelaar J, Chin A, Leer JW. Electron beam irradiation is effective in the treatment of skin carcinomas; a comparison with superficial roentgen therapy. Ned Tijdschr Geneeskd. 1996;140:428–431.

19. Amdur RJ, Kallbauch KJ, Ewald LM, et al. Radiation therapy for skin cancer near the eye: Kilovoltage x-rays versus electrons. Int J Radiat Oncol Biol Phys. 1992;23:769–779.

20. Das JJ, Kase KR, Copeland JF, Fitzgerald TJ. Electron beam modifications for the treatment of superficial malignancies. Int J Radiat Oncol Biol Phys. 1991;21:1627–1634.

21. van Battum LJ, Huizenga H. On the initial angular variances of clinical electron beams. Phys Med Biol. 1999;44:2803–2820.

22. McParland BJ, Cunningham JR, Woo MK. The optimization of pencil beam widths for use in an electron pencil beam algorithm. Med Phys. 1988;15:489–497.

23. Li XA, Rogers DWO. Electron mass scattering powers: Monte Carlo and analytical calculations. Med Phys. 1995;22:531–541.

24. Radiation dosimetry: Electron beams with energy between 1 and 50 MeV. ICRU Report 35 1984; Bethesda, MD: ICRU.