BACKGROUND: Long QT syndromes (LQTS) arise from many genetic and nongenetic causes with certain characteristic ECG features preceding polymorphic ventricular tachyarrhythmias (PVTs). However, how the many molecular causes result in these characteristic ECG patterns and how these patterns are mechanistically linked to the spontaneous initiation of PVT remain poorly understood.

METHODS: Anatomic human ventricle and simplified tissue models were used to investigate the mechanisms of spontaneous initiation of PVT in LQTS.

RESULTS: Spontaneous initiation of PVT was elicited by gradually ramping up $I_{Ca,L}$ to simulate the initial phase of a sympathetic surge or by changing the heart rate, reproducing the different genotype-dependent clinical ECG features. In LQTS type 2 (LQT2) and LQTS type 3 (LQT3), T-wave alternans was observed followed by premature ventricular complexes (PVCs). Compensatory pauses occurred resulting in short-long-short sequences. As $I_{Ca,L}$ increased further, PVT episodes occurred, always preceded by a short-long-short sequence. However, in LQTS type 1 (LQT1), once a PVC occurred, it always immediately led to an episode of PVT. Arrhythmias in LQT2 and LQT3 were bradycardia dependent, whereas those in LQT1 were not. In all 3 genotypes, PVCs always originated spontaneously from the steep repolarization gradient region and manifested on ECG as R-on-T. We call this mechanism R-from-T, to distinguish it from the classic explanation of R-on-T arrhythmogenesis in which an exogenous PVC coincidentally encounters a repolarizing region. In R-from-T, the PVC and the T wave are causally related, where steep repolarization gradients combined with enhanced $I_{Ca,L}$ lead to PVCs emerging from the T wave. Since enhanced $I_{Ca,L}$ was required for R-from-T to occur, suppressing window $I_{Ca,L}$ effectively prevented arrhythmias in all 3 genotypes.

CONCLUSIONS: Despite the complex molecular causes, these results suggest that R-from-T is likely a common mechanism for PVT initiation in LQTS. Targeting $I_{Ca,L}$ properties, such as suppressing window $I_{Ca,L}$ or preventing excessive $I_{Ca,L}$ increase, could be an effective unified therapy for arrhythmia prevention in LQTS.

VISUAL OVERVIEW: A visual overview is available for this article.
WHAT IS KNOWN?

- Spontaneous initiation of arrhythmias in long QT syndromes exhibits genotype-dependent ECG features including T-wave alternans, short-long-short sequence (or a pause).
- R-on-T is the most common ECG phenomenon during ventricular arrhythmia initiation in long QT syndromes (LQTS).
- QT prolongation is a major risk factor of ventricular arrhythmias and sudden cardiac death in congenital and acquired long QT syndromes (LQTS), heart failure, and ischemia. During the last 2 decades, genetic sequencing and molecular studies have revealed a diverse taxonomy of congenital LQTS subtypes, classified by both the specific genetic mutations and the ion channels they affect. Since the discovery of LQTS type 1 (LQT1), 16 distinct subtypes of LQTS have been classified, with the major subtypes being LQT1, LQTS type 2 (LQT2), and LQTS type 3 (LQT3). In addition, many drugs have been identified to prolong QT interval resulting in acquired LQTS.

WHAT THE STUDY ADDS?

- Computer simulations well capture the diverse ECG features and genotype dependence of arrhythmia initiation in LQTS.
- Despite the many different underlying molecular causes of LQTS, a common mechanism that we call R-from-T is likely responsible for arrhythmia initiation in LQTS.
- Based on these new mechanistic insights, targeting L-type calcium current properties such as suppressing window calcium current or preventing excessive calcium current increase could be an effective unified therapy for arrhythmia prevention in patients with LQTS.

In this study, we seek to bridge the gaps between molecular cause, ECG features, and arrhythmia initiation using in silico models of human LQTS. The ECG patterns from our anatomic ventricle simulations well captured the clinical ECG patterns and their genotype specificities. From our anatomic ventricle and simplified tissue simulations of LQT1, LQT2, and LQT3, we obtained the following mechanistic insight: regional action potential duration (APD) prolongation (and thus QT prolongation) increases repolarization gradients, which when combined with enhanced L-type calcium (Ca²⁺) current (I_{Ca,L}) causes the spontaneous genesis of PVCs. Because these PVCs emerge from the repolarization gradient that gives rise to the T wave, we call this mechanism R-from-T, in contrast with the classic explanation of R-on-T mechanism in which an exogenous PVC coincidentally encounters a vulnerable repolarizing region during the T wave, which we call R-to-T. In other words, in R-from-T, the PVC and the T wave are not coincidental but causally related. We further distinguish these 2 mechanisms in detail in Discussion. Because enhanced I_{Ca,L} is required for the R-from-T mechanism, targeting the properties of I_{Ca,L} could prevent PVC regardless of the specific subtype of LQTS.

METHODS

The authors declare that all supporting data are available within the article and its Data Supplement.

Computer Models

The human anatomic ventricle model was adapted from the one previously developed by Ten Tusscher et al.17,18 We added a Purkinje network to the ventricle model (Figure I in the Data Supplement) generated using a method developed by Sahli Costabal et al.19 One-dimensional (1D) cable and 2-dimensional (2D) tissue models were used for mechanistic investigations. All computer simulations were performed on Tesla and GeForce GPUs (NVIDIA Corporation) with software written in the CUDA programming language.
The human ventricular action potential model by O’Hara et al. 20 was used for the ventricular myocytes. The ICa,L steady-state activation and inactivation curves were taken from either the study by O’Hara et al. 20 or Li et al. 21 The human Purkinje action potential model by Stewart et al. 22 was used for the Purkinje network cells. Instead of using detailed ion channel models simulating specific mutations, 23 we modeled LQT1 by removing the slow component of the delayed rectifier potassium current (IKs), LQT2 by removing the fast component of the delayed rectifier potassium (I Kr), and LQT3 by increasing late sodium current (INaL) in the ventricles. Parameters are detailed in the Data Supplement for each type of LQTS. A bulk heterogeneity in the right ventricle was created by adjusting a nonmutated current for each LQTS subtype (Figure II in the Data Supplement), resulting in an APD map agreeing with the ECG-imaging studies of LQTS patients from Vijayakumar et al. 24

Pseudo-ECGs (Figure III in the Data Supplement) were computed 25,26 with the V5 lead shown unless otherwise specified. Further details of the mathematical models, the fiber structure in the ventricles, the Purkinje network, Purkinje cell-myocyte coupling, and ECG computation are presented in the Data Supplement.

Arrhythmia Initiation Protocols

We used 3 protocols to elicit spontaneous initiation of arrhythmias:

1. ICa,L ramp protocol: constant heart rate with a 20-second ICa,L conductance (PCa) ramp (first panel, Figure 2A). The ramp begins at the control value (PCa,control=0.0001 cm/s=1 μm/s) to a specified high value (PCa,H). The heart rate is fixed. This protocol simulates the initial phase of a β-adrenergic surge, when ICa,L is quickly activated but IKs is not yet. 27

2. Pause protocol (LQT2 and LQT3): constant PCa with a pause in the heart rate by a sudden change from 120 to 60 beats per minute.

3. Increasing heart rate protocol (LQT1): constant PCa with the RR interval gradually decreasing from 1000 (60 beats per minute) to 500 ms (120 beats per minute) in increments of 10 ms per beat.

RESULTS

Initiation of Arrhythmias in LQT2

Simulation of the Anatomic Ventricle Model

We first used the PCa ramp protocol (Figure 2A and 2B) to elicit spontaneous initiation of PVT. Figure 2A shows ECGs in the time interval from 10 to 50 s for different PCa,H values, and Figure 2B shows voltage snapshots for PCa,H=2.8 μm/s. Figure 2C shows the ECGs for the pause protocol in which PCa was held at 2.8 μm/s for the whole simulation period. The ECG dynamics from these simulations are summarized as follows:

1. TWA and PVCs: up to Pca,H=1.5 μm/s, the ECG remained in normal sinus rhythm (first ECG). When Pca,H was increased to 1.7 μm/s, TWA occurred (marked as ABAB on the second ECG). When Pca,H was increased to 1.8 μm/s, PVCs occurred (marked by * on the third ECG). These PVCs were always superimposed on the T wave, manifesting as R-on-T. PVCs still preceded the
appearance of PVCs (marked as ABA on the third ECG), with the first PVC occurring on the larger of the alternating T waves.

2. SLS sequence: at $P_{Ca,H} = 1.8 \text{ \mu m/s}$, the first PVC blocks next sinus beat, resulting in a compensatory pause. After this pause and the next sinus beat, a second
PVC occurs resulting in a classic SLS sequence. This ECG pattern repeated as $P_{Ca}$ was held at 1.8 μm/s. When $P_{Ca,H}$ was increased to 2.0 μm/s (fourth ECG), after the first compensatory pause, an alternating interpolated PVC pattern formed where a PVC occurred after every other sinus beat without compensatory pauses—a behavior we call PVC alternans.

3. PVC preceding SLS sequence: when $P_{Ca,H}$ was raised to above 2.5 μm/s, multiple episodes of nonsustained PVT (fifth ECG) and sustained PVT (sixth ECG) occurred. These episodes of PVC were always preceded by an SLS sequence. To reveal how PVCs and PVC occur spontaneously in the heart, we show selected snapshots in a 3-view sequence (Purkinje network voltage, ventricular myocardium voltage, and ventricular excitation wave fronts) for the initiation episode in the $P_{Ca,H}=2.8$ μm/s case (Figure 2B). Focal excitations repeatedly originate from the right ventricle heterogeneity and eventually evolve into a focal-reentrant mixture (see Movie I in the Data Supplement for the entire episode).

4. PVC preceding a pause: we were also able to initiate arrhythmias using the pause protocol. Figure 2C shows an ECG for $P_{Ca}$ held at 2.8 μm/s, in which the heart rate was suddenly decreased from 120 to 60 beats per minute when the heart rate was 120 beats per minute, no TWA or PVCs occurred. After the heart rate was changed to 60 beats per minute, PVC was initiated immediately.

Mechanistic Insights of Arrhythmogenesis From 1D and 2D Tissue Simulations

To better understand the underlying mechanism of arrhythmia initiation in the anatomic ventricle, we carried out additional simulations using 1D cable and 2D tissue models.

In the 1D cable, a region of longer APD was placed in the center by using a smaller $I_{Ks}$ conductance ($G_{Ks}$), paced from the upper end. When $P_{Ca}$=1 μm/s (Figure 3A), the APD was stable in the entire pacing cycle length (PCL) range from 400 to 1600 ms. For $P_{Ca}$=2.0 μm/s (Figure 3B), when PCL was increased to 1000 ms, APD alternans occurred in the center region of the cable but did not generate PVCs (corresponding to TWA in the second ECG in Figure 2A). At PCLs >1150 ms, APD dynamics became more complex and PVCs occurred. For $P_{Ca}$=2.3 μm/s (Figure 3C), when PCL was increased to a value where APD alternans occurred, PVCs also occurred. These APD alternans lead to PVC alternans (corresponding to the PVC pattern seen in the fourth ECG in Figure 2A). At slower PCLs, PVCs occur on every beat. Importantly, these PVCs emerge spontaneously from the repolarization gradient region and propagate only in one direction—a process we call spontaneous unidirectional propagation.

In the 2D tissue, a longer APD region is similarly placed in the center of the tissue (Figure 3D and 3E). The tissue was paced from the left edge, and the PCL was maintained at 700 ms for 20 beats and then suddenly increased to 1000 ms. In the first case, the long APD region is circular (Figure 3D; Movie II in the Data Supplement). At PCL=700 ms, no PVCs occurred. After PCL was increased to 1000 ms, focal excitations began to emerge from the APD gradient region. The excitations propagated unidirectionally (indicated by the white arrows), first to the right, then around the longer APD region before finally colliding and annihilating at the left side, forming a target-like pattern. This repeated to generate a focal train of multiple PVCs. As the PCL was maintained at 1000 ms, multiple such episodes occurred. However, when we changed the shape of the longer APD region into a larger and more elongated geometry (Figure 3E; Movie III in the Data Supplement), the initial focal excitation directly evolved into sustained reentry instead, forming a figure-of-eight reentry since the region was large enough that the tips did not collide and annihilate. This reentry arose directly from spontaneous unidirectional propagation of the PVC itself and was not the result of another exogenous PVC encountering conduction block.

Initiation of Arrhythmias in LQT3

We used the same 2 protocols as in LQT2 to elicit arrhythmias. Figure 4A shows the ECGs for the $P_{Ca}$ ramp protocol. Similar to LQT2, TWA preceded R-on-T PVCs (marked by *), and the first PVC always occurred on the larger of the alternating T wave. Most of the time, episodes of PVC followed SLS sequences (ie, a pause), but in some cases, PVC also occurred immediately following TWA without a pause (third ECG). This case of TWA immediately preceding PVC is similar to the clinical example shown in Figure 1. Sustained ventricular tachycardia occurred at $P_{Ca,H}=3.2$ μm/s (sixth ECG). In Figure 4B, we show selected snapshots in a 3-view mode for the initiation episode in the $P_{Ca,H}=3.2$ μm/s case (see Movie IV in the Data Supplement for the entire episode). The PVCs again emerged spontaneously and propagated unidirectionally from the repolarization gradient region. In this case, the focal excitation traveled around the longer APD region and was able to quickly evolve into a stable reentry, manifesting as a monomorphic ventricular tachycardia. Using other parameters, the resulting arrhythmia could be either monomorphic or polymorphic.

We also elicited arrhythmias using the pause protocol (Figure 4C). With a heart rate of 120 beats per minute, no PVCs or arrhythmias occurred even at $P_{Ca,H}=3.6$ μm/s, but arrhythmias occurred immediately after a sudden decrease in heart rate to 60 beats per minute.

Initiation of Arrhythmias in LQT1

Spontaneous initiation of PVC in LQT1 manifests differently than in LQT2 and LQT3. We first used the $P_{Ca}$ ramp protocol with heart rates of 60 and 120 beats per minute.
minute. Figure 5A shows ECGs at 3 $P_{Ca,H}$ values for both heart rates. At $P_{Ca,H}=2.1 \, \mu m/s$, both ECGs show normal sinus rhythm. When $P_{Ca,H}$ was increased to $3.1 \, \mu m/s$, arrhythmias occurred at 120 beats per minute but not at 60 beats per minute. When $P_{Ca,H}$ was increased further to $4.1 \, \mu m/s$, arrhythmias occurred at both heart rates. Note that in either heart rate, arrhythmias always occurred without a preceding pause or SLS sequence. In addition, no TWA was observed at any $P_{Ca,H}$. Despite these differences from LQT2 and LQT3, the arrhythmias were still initiated with an R-on-T (marked by *). The 3-view snapshots also show focal excitations emerging from
the repolarization gradient region, resulting in PVT (Figure 5B; Movie V in the Data Supplement). PVT was also able to be elicited using the increasing heart rate protocol for certain \( P_{Ca,H} \) values between 3.1 and 4.1 \( \mu m/s \), with an example shown at \( P_{Ca,H} = 4.0 \mu m/s \) (Figure 5C).

Although the presence of \( I_{Ks} \) can explain why arrhythmias tend to occur at slower heart rates in LQT2 and LQT3, it is not clear why a unique SLS sequence occurs in LQT2 and LQT3 but not in LQT1. To understand the underlying mechanism, we carried out single-cell and 1D cable simulations comparing LQT1 and LQT2. Figure 6A shows APD versus \( P_{Ca} \) for LQT1 and LQT2. In the case of LQT1, increasing \( P_{Ca} \) causes APD to increase suddenly to repolarization failure. However, in the case of LQT2, APD increases as a
staircase with incremental transitions. The sudden repolarization failure in LQT1 is due to the fact that peak $I_{Kr}$ does not change with increasing APD since $I_{Ks}$ has already saturated (Figure 6B, top), and, therefore, there is not enough outward current to oppose the increase of $I_{Ca,L}$. On the contrary, when $I_{Ks}$ is present as in LQT2, it does increase with
increasing APD because of its slow activation (Figure 6B, bottom), supplying enough outward current to oppose ICa,L for repolarization. At the tissue scale, repolarization failure in the long APD region causes repetitive firings at both fast and slow heart rates (Figure 6C). Therefore, in LQT1, the sudden transition from a normal action potential to repolarization failure causes the transition from sinus rhythm to repetitive focal firings. Single PVCs with a compensatory pause or SLS sequences do not have a chance to develop because full-blown arrhythmias occur immediately from the first PVC onward. Adding a small amount of IKs back into the LQT1 cell causes a more gradual APD change before reaching repolarization failure, and with enough IKs added back, the response is similar to LQT2 (Figure IV in the Data Supplement). Similarly, in the LQT1 1D cable, after adding a certain level of IKs back, the behavior changed from repolarization failure to distinct PVC alternans. These results imply that when IKs conductance is below a certain threshold, one will observe the typical LQT1 pattern of arrhythmia initiation, otherwise, one will observe the LQT2 behavior.

Reducing Window ICa,L Prevents Arrhythmogenesis in LQTS

Although the modes of spontaneous arrhythmia initiation are genotype dependent, one common requirement is the enhancement of ICa,L. Moreover, the R-on-T focal excitations that initiate the arrhythmias always originate from the repolarization gradient regions, resulting in focal, reentrant, or mixed focal-reentrant arrhythmias. Based on our understanding of the role window ICa,L plays in both early afterdepolarization genesis in single cells and PVC formation in heterogeneous tissue, we hypothesized that reducing the window ICa,L can prevent arrhythmias in LQTS. We reduced the window ICa,L by shifting the steady-state inactivation curve (f∞) as indicated in Figure 7A. The advantage of shifting f∞ (in contrast to ICa,L blockade) is that it does not affect ICa,L in the normal action potential (Figure 7B, left) but can effectively suppress early afterdepolarizations (Figure 7B, right) and PVCs. Left shifting f∞ by 5 mV prevented the arrhythmias that were induced by the Pca ramp protocol in LQT1, LQT2, and LQT3 (Figure 7C). To systematically evaluate the efficacy of this therapeutic strategy, we carried out 1D cable simulations to identify the Pca threshold for PVCs versus the amount of f∞ shift (Figure 7D). In all 3 subtypes of LQTS, a 5-mV shift almost doubled the threshold for arrhythmias. At 8-mV shift, no PVCs were seen even at 6x the control Pca for any LQTS subtype.

DISCUSSION

In this study, we used anatomic human ventricle and simplified tissue models to systematically investigate the mechanisms of spontaneous arrhythmia initiation in LQTS. Our simulations reproduced the characteristic ECG features commonly seen in LQTS patients, including TWA, R-on-T, and SLS sequences leading to PVT in LQT2 and LQT3 and nonpause-dependent initiation of PVT in LQT1. 1D and 2D models further explored the detailed mechanisms of TWA, PVC formation, and initiation of arrhythmias. We showed that although the characteristic ECG features preceding the onset of PVT may vary between the different LQTS genotypes, a common mechanism for PVT initiation may exist, which we call R-from-T. In this R-from-T mechanism, PVCs are generated from increased repolarization gradients (as a result of QT prolongation) with an enhanced ICa,L (such as during a β-adrenergic surge), which then propagate unidirectionally away from the repolarization gradient region. This can generate either target-like excitation patterns resulting in focal arrhythmias or evolve into reentrant arrhythmias depending on the geometry of the tissue heterogeneity. This new understanding leads to a unified therapeutic strategy in which a single intervention of suppressing window ICa,L effectively prevented arrhythmias in multiple LQTS subtypes. Detailed mechanistic insights and implications for clinical arrhythmia prevention are discussed in detail below.

R-From-T as a Common Mechanism of Arrhythmia Initiation in LQTS: R-on-T Revisited

R-on-T is a descriptive term denoting the ECG appearance of an R wave superimposed on a T wave. R waves that occur during the downslope of a T wave have been widely associated with increased arrhythmia risk in a variety of conditions. Here, we discuss our current understanding of the different possible mechanisms by which arrhythmias can spontaneously initiate with the R-on-T phenomenon (Figure 8; Movie VI in the Data Supplement).

The classical mechanistic explanation for arrhythmias initiating as an R-on-T is as follows: when an ectopic PVC from somewhere either in the Purkinje network or ventricular myocardium encounters a refractory region with right timing, unidirectional conduction block can occur, which may then develop into figure-of-eight reentry (Figure 8, left). Because in this scenario the PVC travels and encounters a repolarizing T wave by chance, we call this classic mechanism the R-to-T mechanism.

In the current and our previous studies, we have shown that PVCs can also spontaneously arise from a repolarization gradient via a dynamical instability when ICa,L is significantly enhanced. The PVCs from this mechanism will always appear and coincide during the T wave, also manifesting as R-on-T on ECG. Because these PVCs arise from the repolarization gradient and thus are causally linked with the T wave, we call this new mechanism the R-from-T mechanism (Figure 8, right). Note that in R-to-T, the R wave and T wave are 2 independent events, while in R-from-T, the R wave is caused by the T wave.
In R-from-T, after the PVCs emerge spontaneously from the repolarization gradient region, they propagate unidirectionally away from the gradient—a behavior we call spontaneous unidirectional propagation. Evidence of this type of PVC behavior has been shown in optical mapping experiments of rabbit and canine hearts,\textsuperscript{31,35–37} where spontaneous PVCs would emerge from the steep repolarization gradient region and propagate unidirectionally. This behavior results in distinctly different mechanisms of arrhythmogenesis compared with the classical R-to-T mechanism. First, repeated PVCs can occur by R-from-T,\textsuperscript{31} manifesting as singlets, couplets, or a long train of PVCs, resulting in sustained or nonsustained focal arrhythmias. Second, since the PVC only propagates unidirectionally, it can also evolve directly into reentrant arrhythmias without requiring an additional region of heterogeneity to cause conduction block. Thus, depending on the properties of the heterogeneity, these PVCs can result in focal, reentrant, or mixed focal/reentrant arrhythmias all from the same R-from-T mechanism.
Since the R-from-T PVCs and the subsequent arrhythmias are caused by the same mechanism, a single PVC in this case can be considered as just the shortest possible run of an arrhythmia. Couplets, triplets, trains of PVCs, and the subsequent PVT are just longer runs of arrhythmias from the same underlying instability, which depends on the cellular and tissue properties, as well as the interactions of PVCs with the sinus beats. In this sense, the R-from-T mechanism blurs the line between the usual notions of a distinct trigger and substrate in arrhythmia initiation.
While the R-to-T mechanism is widely considered as the prototypical mechanism of arrhythmogenesis in cardiac diseases in general,\(^3\) it is unknown whether such a mechanism is indeed responsible for the spontaneous initiation of arrhythmias in LQTS. Although the R-to-T mechanism has been reproduced in computer simulations of LQTS using an externally applied premature stimulus (so-called S1S2 protocol),\(^4\) to our knowledge, there is no clear experimental evidence of spontaneous arrhythmias caused by R-to-T in LQTS. On the contrary, several optical mapping experiments of LQTS do show spontaneous unidirectional propagation from the steep repolarization gradient region,\(^3\) consistent with the R-from-T mechanism. Other recent simulation studies\(^3\) have also shown spontaneous initiation of arrhythmias without an external stimulus, while our current study is able to reproduce the characteristic ECG features seen in patients with LQTS and reveals how R-from-T serves as a common mechanism of arrhythmia initiation in different LQTS subtypes.

**Mechanistic Links Between the Characteristic ECG Features and Spontaneous PVT Initiation in LQTS**

TWA and SLS sequences are the major characteristic ECG features known to precede PVT in LQTS, but their detailed relationship is not well understood. Our results from this study offer a deeper explanation through the R-from-T mechanism.

TWA has been widely observed in LQTS\(^4,14-16\) and often precedes the initiation of PVT, either immediately (eg, center bottom in Figure 1)\(^6\) or many hours before a pause-induced arrhythmia. In our \(I_{Ca,L}\) ramp protocol simulations of LQT2 (Figure 2) and LQT3 (Figure 4), TWA was observed just before the appearance of PVCs and PVT. The first PVC during the \(I_{Ca,L}\) ramp always occurred on the larger of the alternating T waves. In most of the cases, PVT initiation was still preceded by an SLS sequence but could also occur immediately following TWA without an SLS sequence (third ECG in Figure 4A). These simulated ECG behaviors agree well with the clinical ECG features seen in patients with LQTS.\(^4,6,16\) PVCs and initiation of PVT also result from enhanced \(I_{Ca,L}\) and slow heart rates but do not necessarily require TWA to occur. The \(I_{Ca,L}\) threshold or the heart rate threshold for TWA is lower than that for PVCs and arrhythmias, which may explain why TWA occurs frequently in LQTS without arrhythmias or can occur long before arrhythmia onset. These insights agree well with the clinical observation that LQTS patients with TWA have a higher incidence of arrhythmias, but QT prolongation is still the primary risk factor.\(^15\)

The SLS sequence or a pause immediately preceding PVT initiation is a unique ECG feature in LQTS, accounting for the majority of PVT initiation patterns.\(^4,10-13,44\) In our anatomic ventricle simulations, almost all PVT episodes were preceded by an SLS sequence in LQT2 and LQT3, but not in LQT1, agreeing with clinical observa-
tions. In our $I_{Ca,L}$ ramp protocol simulations, the SLS sequence appeared naturally as $I_{Ca,L}$ was ramped up. When the first PVC occurs (short), it propagates retrogradely through the Purkinje network, blocking the next sinus beat and resulting in a longer RR interval (long). This increased RR interval further exacerbates the repolarization gradient, leading to another PVC on the next beat (short). Since this pause is longer than the normal sinus RR interval, the repolarization gradient becomes more severe, which can lead to repetitive PVCs or reentrant PVT. The role of the first PVC, whether it arises from R-from-T or any additional mechanisms including delayed afterdepolarizations, Purkinje automaticity, or even heart rate variability (e.g., in Figures 2C and 4C), is to simply set up the long compensatory pause.

Note that our anatomic ventricle simulations capture the wide range of ECG phenomenon in LQTS, including TWA, PVCs, SLS, R-on-T, and PVTs, with only a single intervention, that is, ramping up $I_{Ca,L}$. This suggests that the R-from-T mechanism is a likely candidate for spontaneous arrhythmogenesis in LQTS.

**Genotype-Dependent Onset of PVT: Role of $I_{Ks}$**

Different LQTS subtypes are known to exhibit different genotype-dependent triggers and characteristic ECG features preceding PVT. For example, LQT2 and LQT3 arrhythmias tend to be more bradycardia dependent, whereas in LQT1, this rate dependence is much less sensitive and can even be tachycardia dependent—a feature well captured by our simulations. This can be explained by the well-known effect of the slow transition to the deeper closed states of $I_{Ks}$: a longer diastolic interval will cause fewer channels to be available for immediate opening in the next action potential and thus results in a lower repolarization reserve. However, it is not clearly understood why SLS sequences occur frequently in LQT2 and LQT3 but not in LQT1. This study offers further mechanistic insight.

The effects of slow activation of $I_{Ks}$ on APD have been investigated in general in our previous study and in a recent study by Varshneya et al. As shown in our single-cell and 1D cable results (Figure 6), in the absence of $I_{Ks}$, the action potential tends to exhibit an all-or-none response to increasing $I_{Ca,L}$, that is, the action potential either repolarizes normally or fails to repolarize. But in the presence of $I_{Ks}$, the APD exhibits a more graded response to increasing $I_{Ca,L}$ because of the slow activation of $I_{Ks}$. Therefore, in LQT1, repolarization failure will occur abruptly in the longer APD region once $I_{Ca,L}$ reaches the threshold, directly generating repetitive focal PVCs and causing a sudden transition from sinus rhythm to PVT. In LQT2 and LQT3, however, the APD increases gradually in response to the $I_{Ca,L}$ ramp. When $I_{Ca,L}$ reaches the threshold, only a single PVC is generated, which can result in a compensatory pause and potentiates R-from-T arrhythmogenesis in a pause-dependent manner with an SLS sequence.

Although these genotype-dependent features leading up to PVT appear different, the mechanism of arrhythmia initiation is still the same, that is, R-from-T. Therefore, this study provides important insights that mechanistically link the molecular causes of LQTS to the characteristic ECG features and then these ECG features to a common R-from-T mechanism for spontaneous PVT initiation.

**Implications for Developing a Unified Therapy for PVT Prevention in LQTS**

A major insight from our study is that the R-from-T mechanism may be the final common pathway leading to PVT initiation, regardless of the LQTS genotype. One critical factor for R-from-T was an enhanced $I_{Ca,L}$. It is well known that blocking Ca$^{2+}$ channels has adverse effects of weakening contraction, and thus, Ca$^{2+}$ channel blockers are typically not appropriate for clinical use. In this study, we showed that R-from-T arrhythmogenesis does not occur until $I_{Ca,L}$ is significantly increased above baseline (a 2- to 4-fold increase). Therefore, instead of blocking $I_{Ca,L}$ overall, preventing excessive increase of $I_{Ca,L}$ over baseline can still be effective in preventing R-from-T arrhythmias. This observation agrees with current clinical practice where β-blockers are used as the mainstay arrhythmia prevention therapy in LQTS, since β-blockers can prevent the excessive $I_{Ca,L}$ increase during a sympathetic event, albeit still with notable side effects on heart rate, exercise tolerance, and blood pressure.

In this study, we demonstrated another potential therapy, treating different LQTS subtypes using only a single intervention by reducing the $I_{Ca,L}$ window current with a simple shift in the steady-state inactivation curve ($f_\infty$). In other words, we were able to prevent arrhythmias in LQT1, LQT2, and LQT3, only by targeting the $I_{Ca,L}$ window current. The advantages of this therapeutic strategy include the following: (1) it avoids affecting the normal calcium transient required for contractility as calcium channel blockers would; (2) it does not affect the APD (and thus QT interval) during sinus rhythm, differing from many of the ion channel blockers; and (3) it avoids affecting the heart rate as with β-blockers. Our results demonstrate that this approach was effective, as only a small 5-mV shift in $f_\infty$ doubled the arrhythmia threshold for all LQTS subtypes.

It has been shown that spontaneous Ca$^{2+}$ release can also be a potential mechanism for arrhythmias in LQTS, which does not rely on the $I_{Ca,L}$ window current. However, as demonstrated in the study by Wilson et al., blocking $I_{Ca,L}$ can effectively abolish the spontaneous Ca$^{2+}$ oscillations because of a reduction of the sarcoplasmatic reticulum Ca$^{2+}$ load. Therefore, we predict that blocking window $I_{Ca,L}$ may still indirectly have an effect on arrhythmia suppression, since blocking window $I_{Ca,L}$ in LQTS can also reduce...
the overall sarcoplasmic reticulum Ca²⁺ load. This effect needs to be explored in future modeling studies.

Limitations
For the sake of mechanistic clarity and data availability, some aspects of our models were simplified in as reasonable a manner as possible. The anatomic ventricle model tissue heterogeneity was simulated as a simplified single bulk region to elicit a clearly interpretable initiation of arrhythmias, which may result in T-wave morphologies that differ from real patients. More complicated heterogeneities may result in more mixed cases with different or multiple initiation sites. In addition, interpatient ionic current variability can play important roles in the mode of arrhythmia initiation, which may require population modeling approaches. We also simulated the β-adrenergic surge by only ramping up I_{Ca,L} without any other effects, focusing on the initial phase of sympathetic simulation. In this study, the most extreme congenital LQT1 and LQT2 focusing on the initial phase of sympathetic simulation. In this study, the most extreme congenital LQT1 and LQT2 mutations of zero I_{Ca,L} were simulated, but there are many other possible mutations with partial reduction or trafficking defects instead of complete deficiency, which may result in further mixed or intermediate behaviors. Finally, this study focused on congenital LQT1, LQT2, and LQT3, but the insights into PVT initiation and prevention by targeting I_{Ca,L} could also be applicable to other congenital LQTS and acquired LQTS since the R-from-T mechanism seems invariant to the particular cause of QT prolongation, as long as a repolarization gradient and sufficiently elevated I_{Ca,L} exists. This needs to be verified in other types of congenital LQTS and acquired LQTS in future modeling studies and eventually verified in future experimental and clinical studies.

Conclusions
Despite the complex genetic and nongenetic causes of LQTS and genotype-dependent clinical features, R-from-T offers a promising common mechanism for PVT initiation in LQTS. Because R-from-T arrhythmogenesis is promoted by a steep repolarization gradient and requires an enhanced I_{Ca,L} to occur, targeting I_{Ca,L} properties, such as suppressing window I_{Ca,L} or preventing excessive increase of I_{Ca,L} can be an effective unified therapy for arrhythmia prevention in LQTS.

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Disclosures
None.

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