Three-dimensional versus two-dimensional derived strain echocardiography for assessing right ventricular myocardial deformation in patients with chronic left ventricular heart failure: A proof-of-concept study

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Research article

Keywords: Echocardiography, right ventricular, three-dimensional, myocardial function, strain

DOI: https://doi.org/10.21203/rs.2.23108/v3

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Abstract

Background: A novel three-dimensional echocardiography (3DE)-derived strain analysis software specialized for right ventricular (RV) monitoring is emerging that could definitely evaluate RV free wall and interventricular septum longitudinal strain. The aim of this study was to compare the diagnostic performance in evaluating RV function between 3DE and two-dimensional echocardiography (2DE)-derived longitudinal strain.

Methods: Echocardiographic examinations were performed in 82 patients with RV dysfunction associated with chronic left-sided heart failure and 40 control subjects. RV dysfunction was defined as a 3DE-derived RV ejection fraction (EF) <45%. Both 2DE and 3DE-derived strain analyses were performed in all the patients to measure the longitudinal strain of RV.

Results: 3DE-derived peak systolic longitudinal strain of RV free wall (RV-fwLS) was significantly lower in patients with RV dysfunction compared to control subjects (-14.0±4.1 vs. -26.7±4.7%; p<0.001), and it correlated well with cardiac magnetic resonance-derived RVEF (r=0.74, p<0.001). On receiver operator characteristic analysis, a 3DE-derived RV-fwLS cutoff value of >-21.1% was most useful in identifying patients at higher risk of RV dysfunction (sensitivity: 90% and specificity: 85%), also higher than 2DE-derived strain parameters. Additionally, RV dysfunctional patients with pulmonary hypertension (PH) had significantly reduced 3DE-derived RV-fwLS value than the subgroup without PH (-13.1±3.8 vs. -15.0±4.2; p<0.05).

Conclusion: Assessment of impaired RV systolic function by 3DE-derived longitudinal strain is better than 2DE in chronic left-sided heart failure patients with left ventricular EF <45%. 3DE-derived strain analysis specialized for RV should be considered as a complementary tool for assessing RV function.

Background

Assessment of right ventricular (RV) function has been validated as an important method for predicting clinical outcomes in patients with chronic left-sided heart failure, and even superior to left ventricular ejection fraction (LV-EF) [1, 2]. However, it is difficult to generate an accurate echocardiographic evaluation of RV myocardial function due to the complex anatomy and morphology involved [3]. Conventional echocardiographic parameters such as tricuspid annular plane systolic excursion (TAPSE) and RV fractional area change (FAC) are widely used in clinical practice. However, both of these methods have intrinsic shortcomings, which limit their specificity and reliability [4, 5].

Due to the longitudinal alignment of deep muscle fibers in RV, longitudinal shortening is a major contributor to RV systolic function. So longitudinal strain parameters can provide additional information about RV systolic function, enabling more accurate evaluation [3, 6, 7]. Many techniques have been introduced to quantitatively evaluate RV myocardial function by longitudinal strain. Two-dimensional (2D) speckle tracking echocardiography being used to evaluate LV systolic function, known for its ability to detect altered myocardial mechanics under different cardiovascular conditions, has already been...
applied to myocardial deformation assessments of RV [8-10]. However, RV deformation analyses based on two-dimensional echocardiography (2DE) are limited to be used in 2D planes in which volumetric assumption of the authentic morphology cannot be avoided.

Most recently, three-dimensional (3D) speckle tracking echocardiography originally developed for LV assessment was used to assess RV function with limitation in defining the location of the free wall-septal border [9, 12, 13]. The newly emerging three-dimensional echocardiography (3DE)-derived strain analysis particularly for RV have an evident advantage in its ability to recognize RV free wall and interventricular septum, is expected to provide more comprehensive assessment of RV systolic function [14].

In light of the potential technical advantages of this technology, we hypothesized that 3DE-derived longitudinal deformation parameters were more accurate than 2DE in assessing RV myocardial function. The aims of this study were to evaluate their diagnostic value in identifying patients with RV dysfunction as defined by the standard of 3DE-derived RVEF <45% [4], and determined whether 3DE-derived longitudinal strain of RV correlates to cardiac magnetic resonance (CMR)-derived RVEF. Additionally we assessed whether there existed differences in the magnitude of 3DE-derived longitudinal deformation parameters of RV between RV dysfunctional patients with and without pulmonary hypertension (PH).

**Methods**

The study complied with the Declaration of Helsinki and was approved by the Ethics Committee of Harbin Medical University. All patients signed a written informed consent form prior to participating in the study.

**Study Population**

From a large group of consecutive patients referred to our echocardiography center, 117 patients met with the diagnostic criteria of left-sided heart failure (LVEF <45%) were recruited. Patients with atrial fibrillation, primary pulmonary hypertension, congenital heart disease or had undergone previous tricuspid valve surgery were excluded. Subjects with any obvious abnormalities of valvular structure or LV and/or RV geometry and function were also excluded. Sixteen (13.7%) patients were excluded due to poor image quality (including poor acoustic windows, image artefacts, and enlarged RV being too large to fit entirely into the 3D full volume) or poor tracking.

An additional 40 healthy subjects with normal LV function, matched for gender and age, referred to our hospital for physical examination were prospectively enrolled as a control group. They volunteered to take routine examinations as needed, and were eligible as having no coronary artery disease documented by invasive coronary angiography or computed tomography angiography.

Finally, 82 patients with RV dysfunction (defined as 3DE-derived RVEF <45%) and 40 healthy subjects were included. Among the patients with RV dysfunction, a cutoff value of 35 mmHg [15] pulmonary pressure during systole was used to define PH. Of the 82 patients, 40 (48.8%) had PH and 42 (51.2%) did not.
Traditional echocardiographic measurements

A complete transthoracic echocardiogram was performed using a Vivid E9 scanner (GE Healthcare, Horten, Norway) in accordance with the guidelines for the examination of RV [4]. All echocardiographic measurements were processed according to the current guidelines [16]. The myocardial performance index (MPI) is a calculation based on tissue Doppler velocities from RV: (isovolumic relaxation time - isovolumic contraction time) / RV ejection time. Conventional color Doppler imaging was used to grade the severity of tricuspid regurgitation semiquantitatively on a 4-point scale (normal, mild, moderate and severe) method by evaluating the ratio of tricuspid regurgitation jet area to right atrial area [17]. The systolic pulmonary pressure was assessed using tricuspid regurgitation peak velocity (performed by the modified Bernoulli equation) and right atrial pressure (estimated from the inferior vena cava diameter using a long-axis subxiphoid view and its response to inspiration).

2DE-derived strain analysis

2DE-derived RV longitudinal strain analysis was offline assessed by the dedicated Echo-PAC version 201 software (GE Healthcare). Three consecutive heart cycles of modified apical 4-chamber images focus on RV were digitally saved for the subsequent analysis. Adjust the frequency, depth, and sector width to obtain the optimal frame rate of 60 to 90 frames/s. All data was analyzed by an investigator who was blinded to the individuals' baseline clinical information. The investigator manually traced the endocardial contours and set the width to fit for the RV wall to obtain optimal tracking data. The region of interest consists of six segments (RV free wall and interventricular septum at three levels), which were automatically tracked frame by frame throughout the cardiac cycle. Peak systolic longitudinal strain of RV free wall (RV-fwLS) and peak systolic longitudinal strain of interventricular septum (sLS) were calculated by averaging peak systolic values in the three RV free wall segments or three interventricular septal segments, respectively.

3DE-derived strain analysis

3D data were acquired with a fully sampled matrix-array V4 transducer. Consecutive 4-beat electrocardiographically triggered capture was acquired from a modified apical 4-chamber view focused on RV to enable generation of the full-volume data during breath hold. Special attention was paid to ascertain the pyramidal volume covered the entire RV myocardium with a scan angle as narrow as possible. Image optimization included adjustments of volume size, frame rate, gain, compression and depth. Mean volumetric frame rate was 21 ± 6 volumes/s in this study. The quality of the acquisitions was verified for each individual to ensure that optimal imaging had been done for the entire RV, without obvious stitching artifacts in the multislice display mode. 3D full-volume data were analyzed by a blinded investigator using the 4DAutoRVQ package (Echo-PAC version 201). Manual adjusted the sample lines to determine the axes of LV and RV chamber, the boundaries of aortic annulus and endocardium of RV in an end-diastolic frame of a quad view. Subsequently, three short-axis and one long-axis views of RV were generated to be used to manually delineate the detailed endocardium of RV in end-systole and end-diastole. The images that ultimately failed to track due to the suboptimal image quality were removed.
from the further analysis. The software then automatically traced the endocardial border and analyzed 3D tracking frame-by-frame, 3DE-derived volumetric parameters of RV, RVEF, RV-fwLS and RV-sLS were then generated. (Figure 1)

**CMR measurements**

CMR examinations were performed in 32 out of 82 patients with left-sided heart failure using a 1.5-T scanner (Siemens AG, Erlangen, Germany) with a phased-array cardiovascular coil. Eight to sixteen contiguous short-axis slices, paralleled to the plane of the atrioventricular valves, getting from the base to apex of the heart were obtained in each patient to generate the 2D steady-state free precession cine imaging. Slice thickness was dependent on patient size. RV volumetric analysis was then performed by two investigators blinded to the echocardiographic analysis. In each short-axis slice that encompassed the RV, the RV endocardial contour was manually traced at the end-diastolic frame and end-systolic frame. By the disc summation method, the RV end-diastolic volume (RVESV) and end-systolic volume (RVESV) were generated. RVEF was then calculated by the standard formula.

**Statistical analysis**

Statistical analyses were performed using Medcalc version 15.2. The normal distribution of each parameter was explored by the Kolmogorov-Smirnov test. Continuous data were expressed as the mean ± standard deviation. Categorical data were expressed as numbers and percentages. The two groups were compared using independent student $t$-test, paired $t$-test, chi-square tests, Fisher’s exact test or Mann-Whitney $U$ test depending on the type and distribution of the data. Correlations between two echocardiographic parameters were assessed with Spearman correlation coefficient. Receiver operating characteristic (ROC) curves and their area under the curve (AUC) were calculated to identify the diagnostic accuracy of 2DE and 3DE-derived RV deformation parameters for detection of patients with impaired RV systolic function. Then, we used the ROC curves to determine cutoff levels of corresponding sensitivity and specificity for the above-mentioned variables. AUC values were compared using the method proposed by DeLongs’ [18]. Univariate and multivariate linear regression analyses were then performed to detect the independent correlates that would affect 3DE-derived RV-fwLS in the total study population. All parameters influencing the RV contractile function were selected for linear regression analysis; those parameters with $P$ values <0.05 in univariate analyses were entered into the multivariate model to complete the stepwise forward multiple regression analysis. Bland-Altman analysis was used to estimate mean intra-/interobserver differences from the corresponding repeated measurements, and reproducibility was assessed using intraclass correlation coefficients (ICCs) with 95% confidence intervals. $P$<0.05 was considered significant.

**Results**

**Baseline clinical characteristics**
As shown in table 1, both groups had similar age ranges (58.7±14.2 vs. 55.2±7.0, p=0.067) and sex distributions (male: 76.8% vs. 60.0%, p=0.054). In our study cohort, 46 (56.1%) RV dysfunctional patients were concomitant with diabetes mellitus and/or hypertension. There were also no differences in clinical characteristics of all RV dysfunctional patients with and without performing CMR (table 2).

**Conventional echocardiographic parameters**

The table 3 listed all the values of conventional echocardiographic parameters. Compared to the controls, the patients with RV dysfunction had significantly lower TAPSE, RV-FAC and RV s’ (all p<0.001). By contrast, the MPI were higher in RV dysfunction patients (p<0.001). Among the patients with RV dysfunction, the differences of parameters, as the TAPSE and RV-FAC, were still significant between the subgroups with and without PH (all p<0.05). However, there was no statistical differences in the parameters of RV s’ or MPI between these two subgroups (all p>0.05).

**Strain parameters**

Comparison of strain parameters between each two groups were summarized in Table 4. As seen in the table, the values of 3DE-derived RV-fwLS and sLS in the normal subjects were -26.7±4.7% and -15.5±4.3 %, respectively. The longitudinal strain of interventricular septum, using both 2DE and 3DE methods, were consistently lower than the corresponding values in free wall of RV for all the subjects (all p<0.001). As expected, the longitudinal strain values were severely reduced in patients with RV dysfunction than control group (all p<0.001), take 3DE-derived RV-fwLS (-14.0±4.1 vs. -26.7±4.7%; p<0.001) for instance. The RV dysfunction patients with PH had greater impairments of RV function assessed by 2DE and 3DE-derived RV-fwLS than patients without PH (all p<0.05). Among the patients with RV dysfunction, we found that there existed no difference between subgroups with ischemia and nonischemic cardiomyopathy in the deformation parameters of 2DE- and 3DE-derived RV-fwLS (-16.1±6.0 vs. -15.2±6.9%, -14.4±4.3 vs. -13.6±3.7%, all p>0.05). For the overall study population, we found that the values of 3DE-derived deformation parameters of RV showed relatively lower in magnitude than the corresponding 2DE-derived deformation parameters: RV-fwLS (-18.2±7.3 vs. -19.4±7.9%, p=0.016), sLS (-10.0±5.3 vs. -10.3±6.4%, p=0.377).

The figure 2 showed the ROC analyses of 2DE and 3DE-derived RV-fwLS to predict the patients with RV dysfunction. We detected that both 2DE and 3DE-derived RV-fwLS had good diagnostic accuracies for detection of patients with impaired RV dysfunction, while 3DE-derived RV-fwLS (AUC=0.975) showed higher predictive power than 2DE-derived RV-fwLS (0.930) (p<0.05). With a cutoff value of >-21.1% for 3DE-derived RV-fwLS presented optimal sensitivity of 90% and specificity of 85% to identify patients who are at a greater risk of RV dysfunction. On ROC analysis, we also discovered that 3DE-derived RV-fwLS had a good predictive ability to detect RV dysfunctional patients with PH (AUC=0.638), a cutoff value of >-14.13% showed the best combination of sensitivity of 70% and specificity of 52%. Moreover, 2DE-derived RV-fwLS (AUC=0.648) showed a relatively higher predictive performance than 3DE-derived RV-fwLS, and the difference came to no significance (p=0.882).
**Correlation analysis**

The correlations of all the echocardiographic parameters to CMR-derived RVEF were presented in figure 3. We could know from the figure that all functional parameters were correlated significantly to CMR-derived RVEF \((p<0.001)\). Among the parameters of RV contraction, only 3D-derived RV-fwLS showed a good correlation to CMR-derived RVEF \((r=-0.747, p<0.001)\). The correlation coefficient between 3D-derived sLS and CMR-derived RVEF was moderate \((r=-0.458, p=0.008)\), weaker than 3D-derived RV-fwLS. It was also found that 3D-derived RV-fwLS presented higher correlations to CMR-derived RVEF than any of the following 2D-derived deformation parameters: RV-fwLS \((r=-.527, p=0.002)\), sLS \((r=-.366, p=0.039)\). Meanwhile, we discovered that the conventional echocardiographic parameters (as TAPSE, RV-FAC, RV s’ or MPI) showed lower correlations to CMR-derived RVEF than either the 2D or 3D-derived deformation parameters of RV. As expected, 3D-derived RVEF had strong correlation with CMR-derived RVEF \((r=0.855, p<0.001)\).

Significant univariate and multivariate correlates of 3D-derived RV-fwLS in all the study subjects were shown in Table 5. The presence of diabetes, hypertension, hyperlipidemia, diminished LV end-diastolic volume (EDV), and lower TAPSE were all significant univariate associates of 3D-derived RV-fwLS. Multivariate regression analysis using a stepwise forward algorithm demonstrated that combining with diabetes, hypertension, lower LVEDV and TAPSE were the independent determinants of 3D-derived RV-fwLS.

**Observer reproducibility**

Figure 4 exhibited the intraobserver and interobserver variability of measurements of 3D-derived RV deformation parameters by Bland-Altman graphs. As presented in the figure, intra- and interobserver reproducibility was excellent for both 3D-derived deformation parameters of RV (ICC>0.9). Intraobserver reproducibility for echocardiographic parameters of 3D-derived RV-fwLS and sLS was 0.92 and 0.93 as assessed by ICC, and interobserver reproducibility for 3D-derived RV-fwLS and sLS was 0.92 and 0.90, respectively. Intraobserver reproducibility for 2D-derived RV-fwLS and sLS was 0.91 and 0.89, and interobserver reproducibility for 2D-derived RV-fwLS and sLS was 0.92 and 0.91, respectively.

**Discussion**

The following conclusions were reached based on the study results evaluated above: 1) The 3D-derived RV-fwLS was an appropriate parameter for predicting patients with impaired RV systolic function and more powerful than 2D-derived RV-fwLS. 2) There were moderate to good correlations of 3D-derived RV longitudinal strain to CMR-derived RVEF, and the relation of 3D-derived RV-fwLS to CMR-derived RVEF was greater than other measurements of RV systolic function. 3) RV dysfunctional patients with PH showed significant lower values in 3D-derived RV-fwLS than patients without PH.

The RV performance is increasingly being recognized as a major predictor of long-term outcomes in various pathological conditions [19-21]. An analysis of RV performance based on geometric models in
conventional 2DE method that could not assess the anterior and posterior walls or outflow tract of RV adequately, as these territories are poorly visualized in 2D planes. Given the irregular shape of RV, 3DE-derived strain parameters could avoid this shortcoming to better reflect the true contractive condition of RV. To the best of our knowledge there is, as of yet, no published research assessing RV-fwLS in a 3DE environment for patients with RV dysfunction referred to chronic left-sided heart failure. We reported that 3DE-derived RV-fwLS has a better correlation to CMR-derived RVEF, and could detect more deformational features useful in identifying patients with RV dysfunction than 2DE-derived RV-fwLS. However, Smith et al. demonstrated 3DE-derived global longitudinal strain showed only moderate correlation to 3DE-derived RVEF, it might because of different system and vendor [13].

We observed that the correlation of 2DE or 3DE-derived RV longitudinal strain to CMR-derived RVEF was moderate to good. The RV myocardium mainly consists of myocardial fibers with the epicardial circumferential to oblique alignment and the subendocardial longitudinal alignment [3]. Longitudinal contraction contributes more to RV systolic function than transverse shortening, accounting for nearly 80% of overall RV function. Therefore, the dominant RV myocardial contraction is longitudinal direction [6, 7]. Our study also indicated that the magnitude of the longitudinal strain in patients with RV dysfunction was significantly reduced relative to control subjects. In the present study, the variables of RV end-diastolic pressure and tricuspid regurgitation were not taken into analysis of the predictors of 3DE-derived RV-fwLS. In fact, RV strain parameters are less load-dependent [4]. Meanwhile, the reference values of 3DE-derived longitudinal strain of RV should be established in subsequent studies.

Both ventricles share the oblique fibers in the interventricular septum, which may contribute to their independent contractions [22]. Owing to this important physiologic coaction between LV and RV, the contractile performance of RV is closely linked to the global performance of LV. In our study population, all RV dysfunctional patients were associated with chronic left heart failure. This might weaken the diagnostic accuracies of the corresponding deformation parameters in interventricular septum to discover patients with RV dysfunction. Furthermore, the LV becomes more spherical and interventricular septal myocardial fibers become less oblique because of chronic left heart failure, reducing their mechanical advantage to reflect the longitudinal function. In contrast, the RV-fwLS could analyze the RV mechanism free of influence from LV, are expected to provide more information for the actually contractive condition of RV. In our opinion, it was not appropriate to include the interventricular septum for calculating the global longitudinal strain of RV, as its inclusion would inevitably taint the data for RV analysis.

Along with the findings by Giusca et al. [23] and Wald et al. [24], we also found that conventional RV measurements (such as TAPSE or FAC) had relatively lower correlations to CMR-derived RVEF than RV deformation parameters. TAPSE is easily limited by regional abnormalities in the RV free wall tethering or tricuspid regurgitation, and RV-FAC has a major shortcoming of inter-measurement variability caused by its high dependence on the specific imaging plane. It is obvious that underestimations of TAPSE and RV-FAC could result from its load dependency [4]. Overestimation of TAPSE may be caused by an increasing variability of the apical rotation [5] or the influence of medical therapy on RV regional motion to interfere
its measurements. Nevertheless, RV free wall longitudinal strain is theoretically angle-independent and less susceptible to be influenced by cardiac translational motion, and as such may provide more accurate information concerning RV deformation pattern. Carluccio et al. also discovered that 2DE-derived RV-fwLS could provide incremental prognostic information in heart failure patients with reduced LVEF and preserved TAPSE [25].

In our study cohort, patients with RV dysfunction were divided into two subgroups (those with and without PH) according to the aforementioned cutoff value. RV dysfunctional patients with PH presented with significantly lower magnitudes of longitudinal strain in RV free wall. Increased LV filling pressures could lead to increased pulmonary artery pressure and further impair RV function by increasing the afterload. Our findings supported that 2DE or 3DE-derived RV-fwLS could identify a more advanced stage of cardiopulmonary involvement in patients associated with chronic left heart disease. Prior studies have showed that 2DE-derived RV longitudinal strain could help to predict morbidity and mortality in patients with PH [15, 20]. We hope to explore the potential ability of 3DE-derived RV-fwLS to predict prognosis among these patients in our future studies.

Limitations

Several limitations of the current study should be noted. Firstly, this was a single-territory study only with a small number of subjects, so further studies with a larger amount of subjects are needed to confirm our preliminary findings. Secondly, CMR has been considered as the gold standard for determining RV volumes and RVEF, this modality is limited by its high expense and low availability. However, CMR examinations were not available to all the subjects in this study, we also discovered that there was no difference in the clinical and conventional echocardiographic baseline data between subgroups with and without taking this examination. Thirdly, a portion of subjects in our study had been diagnosed with diabetes mellitus or hypertension which could potentially affect RV function. While excluding these subjects from the comparison did not alter the analysis of RV functional parameters between RV dysfunctional patients and control subjects. Fourthly, we did not assess 3D-derived RV myocardial deformation in radial and circumferential directions in this study. In fact, 3DE-derived radial and circumferential strains of RV were not analyzed owing to methodological limitations of this technology. Longitudinal shortening of the RV has already been shown to be a more important contributor to the RV systolic function compared to circumferential shortening [26]. Fifthly, a small portion of patients with preserved RV function and chronic left heart failure were excluded from the further research, so the results were non suitable to this subgroup, and our further study will expand the sample size to testify the feasibility of 3DE-derived strain analysis in this subgroup. Finally, our study subjects featured different types of etiologies, a larger study population with a pure etiology will be required to validate our findings.

Conclusions

We discovered that impaired RV systolic function assessed by 3DE-derived longitudinal strain is better than 2DE in chronic left-sided heart failure patients with LVEF <45%. 3DE-derived RV-fwLS outperformed
most of currently recommended variables and other deformation parameters to have the highest
correlation to CMR-derived RVEF, and it also could provide additional information for detecting RV
dysfunctional patients with secondary PH. Therefore, our findings supported that the new advent 3DE-
derived strain analysis specialized for RV could be a reliable complementary tool for echocardiographic
assessment of RV systolic function more accurately, which might be further used to identify subclinical
RV dysfunction patients that need additional clinical management.

Declarations

Ethics approval and consent to participate

The study complied with the Declaration of Helsinki and was approved by the Ethics Committee of Harbin
Medical University. All patients signed a written informed consent form prior to participating in the study.

Consent for publication

Not applicable.

Availability of data and materials

All data generated or analysed during this study are included in this published article.

Competing interests

The authors declare that they have no competing interests.

Funding:

Not applicable.

Authors’ contributions:

Concept/design: Tian JW, Du GQ, Gao F and Liu C; Data collection: Gao F, Liu C, Guo Q, Jiang SQ, Wang
ZZ, Liu L, Li HR, Du GQ and Tian JW; Data analysis/interpretation: Gao F, Liu C, Guo Q, Jiang SQ, Wang
ZZ, Liu L, Li HR; Drafting article: Gao F and Liu C; Critical revision of article: Gao F and Liu C; Statistics:
Liu C; Approval of article: Tian JW and Du GQ.

Acknowledgements:

Not applicable.

Abbreviations

2D - Two-dimensional
3D - Two-dimensional

AUC - Area under the curve

CMR - Cardiac magnetic resonance

EDV - End-diastolic volume

EF - Ejection fraction

ESV - End-systolic volume

FAC - Fractional area change

ICCs - Intraclass correlation coefficients

LV - Left ventricular

MPI - Myocardial performance index

PH - Pulmonary hypertension

ROC - Receiver operating characteristic

RV - Right ventricular

RV-fwLS - Peak systolic longitudinal strain of RV free wall

s’ - Peak systolic velocity of tricuspid annular

sLS - Peak systolic longitudinal strain of interventricular septum

TAPSE - Tricuspid annular plane systolic excursion

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Tables
Table 1 Clinical baseline characteristics

| Parameters                        | RV dysfunction (n = 82) | Control group (n = 40) | P value |
|----------------------------------|------------------------|------------------------|---------|
| Age, years                       | 58.7 ± 14.2            | 55.2 ± 7.0             | 0.067   |
| Male, n (%)                      | 63 (76.8)              | 24 (60.0)              | 0.054   |
| Heart rate, beats/min            | 89.5 ± 17.8            | 72.1 ± 7.5             | <0.001  |
| BMI, kg/m²                       | 40.5 ± 6.2             | 37.6 ± 5.2             | 0.013   |
| Risk factors, n(%)               |                        |                        |         |
| Diabetes mellitus                | 18 (22.0)              | 0 (0)                  | 0.001   |
| Hypertension                     | 39 (47.6)              | 1 (2.5)                | <0.001  |
| Hyperlipidemia                   | 20 (24.4)              | 0 (0)                  | <0.001  |
| Smoker                           | 30 (36.6)              | 7 (17.5)               | 0.031   |
| New York Heart Association       |                        |                        |         |
| Functional class, n (%)          |                        |                        |         |
| I                                | 0 (0)                  | -                      | -       |
| II                               | 4 (4.9)                | -                      | -       |
| III                              | 26 (31.7)              | -                      | -       |
| IV                               | 52 (63.4)              | -                      | -       |
| Clinical underlying etiology     |                        |                        |         |
| diagnosis of heart failure, n (%)|                        |                        |         |
| Ischemic heart disease           | 47 (57.3)              | -                      | -       |
| Cardiomyopathy                   | 25 (30.5)              | -                      | -       |
| Valvular heart disease           | 6 (7.3)                | -                      | -       |
| Hypertension                     | 4 (4.9)                | -                      | -       |

RV = right ventricular; BMI = body mass index.

Values are mean ± SD or n (%). P < 0.05 was considered significant. Statistical significance are in boldface type.

Table 2 Clinical baseline and echocardiographic parameters between RV dysfunctional patients with and without performing CMR
| Parameters            | CMR + (n = 32)          | CMR - (n = 50)          | P value |
|-----------------------|-------------------------|-------------------------|---------|
| Age, years            | 55.7 ± 15.0             | 60.6 ± 13.4             | 0.129   |
| Male, n (%)           | 26 (81.3)               | 37 (74.0)               | 0.488   |
| Heart rate, beats/min | 89.2 ± 15.5             | 89.7 ± 19.2             | 0.893   |
| BMI, kg/m²             | 41.2 ± 5.9              | 40.0 ± 6.4              | 0.013   |
| Risk factors, n(%)    |                         |                         |         |
| Diabetes mellitus     | 8 (25.0)                | 10 (20.0)               | 0.594   |
| Hypertension          | 14 (43.8)               | 25 (50.0)               | 0.580   |
| Hyperlipidemia        | 7 (21.9)                | 13 (26.0)               | 0.671   |
| Smoker                | 8 (25.0)                | 22 (44.0)               | 0.081   |
| BNP, pg/ml            | 8463.9 ± 9477.5         | 10421.6 ± 14257.1       | 0.495   |
| LV functional parameters |                       |                         |         |
| LVEDV, ml             | 211.8 ± 76.0            | 195.4 ± 77.5            | 0.347   |
| LVESV, ml             | 146.8 ± 72.0            | 132.5 ± 62.2            | 0.341   |
| LVEF, %               | 30.4 ± 9.8              | 33.6 ± 10.1             | 0.155   |

CMR = cardiac magnetic resonance; RV = right ventricular; BMI = body mass index; BNP = brain natriuretic peptide.

Values are mean ± SD or n (%). P < 0.05 was considered significant. Statistical significance are in boldface type.

Table 3 Conventional echocardiographic parameters from all subjects
| Parameters                          | RV dysfunction (n = 82) | Control group (n = 40) | P value |
|-----------------------------------|------------------------|------------------------|---------|
| **LV functional parameters**      |                        |                        |         |
| LVEDV, ml                         | 201.8 ± 76.9           | 91.2 ± 18.1            | <0.001  |
| LVESV, ml                         | 138.1 ± 66.1           | 29.3 ± 7.6             | <0.001  |
| LVEF, %                           | 32.4 ± 10.0            | 67.8 ± 5.8             | <0.001  |
| **Right heart functional parameters** |                        |                        |         |
| RV Basal diameter, mm             | 34.7 ± 6.7             | 29.3 ± 5.1             | <0.001  |
| RV Longitudinal diameter, mm      | 73.7 ± 9.7             | 65.2 ± 8.9             | <0.001  |
| TAPSE, mm                         | 15.1 ± 3.3             | 21.9 ± 2.9             | <0.001  |
| RVEDA, cm²                        | 19.8 ± 5.5             | 15.8 ± 3.4             | <0.001  |
| RVESA, cm²                        | 14.2 ± 5.3             | 8.7 ± 2.5              | <0.001  |
| RVFAC, %                          | 29.6 ± 12.5            | 45.8 ± 7.2             | <0.001  |
| RV S', cm/s                       | 9.9 ± 3.0              | 12.3 ± 2.0             | <0.001  |
| MPI, %                            | 44.8 ± 8.2             | 38.9 ± 8.0             | <0.001  |
| RA diameter, mm                   | 33.8 ± 7.2             | 30.9 ± 4.7             | 0.021   |
| RVEDV, ml                         | 62.7 ± 26.5            | 39.6 ± 11.1            | <0.001  |
| RVESV, ml                         | 43.5 ± 19.7            | 17.8 ± 6.6             | <0.001  |
| RVEF, %                           | 31.5 ± 6.4             | 53.4 ± 4.9             | <0.001  |
| **Tricuspid regurgitation**       |                        |                        | <0.001  |
| No, n(%)                          | 0 (0)                  | 4 (10.0)               |         |
| Mild, n(%)                        | 28 (34.1)              | 36 (90.0)              |         |
| Moderate, n(%)                    | 10 (12.2)              | 0 (0)                  |         |
| Severe, n(%)                      | 44 (53.7)              | 0 (0)                  |         |

RV = right ventricular; LV = left ventricular; EDV = end-systolic volume; ESV = end-diastolic volume; EF = ejection fraction; TAPSE = tricuspid annular plane systolic excursion; EDA = end-systolic area; ESA = end-diastolic area; FAC = fractional area change; s’ = peak systolic velocity of tricuspid annular; MPI = myocardial performance index; RA = right atrium.

Values are mean ± SD or n (%). P < 0.05 was considered significant. Statistical significance are in boldface type.
Table 4 Strain parameters

| Parameters | All subjects | RV dysfunction (n = 82) | Control group (n = 40) | P value | Without PH (n = 42) | PH (n = 40) | P value |
|------------|--------------|------------------------|-----------------------|---------|-------------------|------------|---------|
| 2DE-derived strain parameters, % | | | | | | | |
| 2DE-derived RV-fwLS | -15.7 ± 6.3 | -27.1 ± 4.8 | <0.001 | -17.3 ± 7.1 | -14.0 ± 5.1 | 0.020 |
| 2DE-derived sLS | -6.8 ± 4.1 | -17.6 ± 3.4 | <0.001 | -7.5 ± 4.8 | -6.0 ± 3.0 | 0.097 |
| 3DE-derived strain parameters, % | | | | | | | |
| 3DE-derived RV-fwLS | -14.0 ± 4.1 | -26.7 ± 4.7 | <0.001 | -15.0 ± 4.2 | -13.1 ± 3.8 | 0.036 |
| 3DE-derived sLS | -7.3 ± 3.3 | -15.5 ± 4.3 | <0.001 | -7.6 ± 3.6 | -6.9 ± 2.9 | 0.300 |

RV = right ventricular; PH = pulmonary hypertension; 2DE = two-dimensional echocardiography; 3DE = three-dimensional echocardiography; RV-fwLS = peak systolic longitudinal strain in free wall of right ventricle; sLS = peak systolic longitudinal strain in ventricular septum.

Values are mean ± SD. P < 0.05 was considered significant. Statistical significance are in boldface type.

Table 5 Univariate and multivariate linear analysis for 3DE-derived RV-fwLS in all the study subjects
| Variable        | Univariate |                                      |       |       | Multivariate |                                      |       |       |
|-----------------|------------|---------------------------------------|-------|-------|--------------|---------------------------------------|-------|-------|
|                 | R          | 95% CI                                | P     | 95% CI| P            | 95% CI                                | P     |       |
| Age             | 0.11       | -0.067-0.284                          | 0.219 | -     | -            | -                                    | -     |       |
| BMI             | 0.18       | -0.001-0.344                          | 0.051 | -     | -            | -                                    | -     |       |
| Diabetes        | 0.33       | 0.159-0.477                           | <0.001| 0.100 | 0.003        | 0.439                                 |       |       |
| Hypertension    | 0.38       | 0.218-0.523                           | <0.001| 0.043 | 0.016        | 0.391                                 |       |       |
| Hyperlipidemia  | 0.23       | 0.059-0.395                           | 0.009 | -0.099| 0.363        | -0.265                                |       |       |
| Smoking         | 0.16       | -0.021-0.326                          | 0.083 | -     | -            | -                                    | -     |       |
| LVEDV           | 0.58       | 0.445-0.685                           | <0.001| 0.299 | <0.001       | 0.591                                 |       |       |
| TAPSE           | -0.71      | -0.786 to -0.605                      | <0.001| -0.693| <0.001       | -0.449                                |       |       |

All abbreviations are as shown in Table 1 or Table 2.

\( P < 0.05 \) was considered significant. Statistical significance are in boldface type.

**Figures**
Figure 1

Example of 3DE-derived strain analysis for RV in a patient with RV dysfunction (a-d) manual tracing the true RV endocardial border in three short and one longitudinal views during end-diastole; (e) 3DE-derived RV reconstruction image seen in front view with listed corresponding contractive function parameter values. 3DE = three-dimensional echocardiography; RV = right ventricular; EDV = end-diastolic volume; ESV = end-systolic volume; SV = stroke volume; EF = ejection fraction; RVLS, peak systolic longitudinal strain of right ventricle.
Figure 2

ROC analyses for the ability of 3DE- and 2DE-derived RV-fwLS to identify patients with RV dysfunction. The analyses included all the study subjects (n=122). 3DE = three-dimensional echocardiography; 2DE = two-dimensional echocardiography; RV-fwLS = peak systolic longitudinal strain in free wall of right ventricle.
**Figure 3**

Correlation analyses between all measurements of RV systolic function with CMR-derived RVEF. CMR = cardiac magnetic resonance; EF = ejection fraction; TAPSE = tricuspid annular plane systolic excursion; RV = right ventricular; FAC = fractional area change; s' = peak systolic velocity of tricuspid annular; MPI = myocardial performance index; 2DE = two-dimensional echocardiography; 3DE = three-dimensional
echocardiography; RV-fwLS = peak systolic longitudinal strain in free wall of right ventricle; sLS = peak systolic longitudinal strain in ventricular septum. P < 0.05 was considered significant.

Figure 4

Bland–Altman agreement plots The figures exhibiting the mean differences and 95% limits of agreement for repeated measurements of 3DE-derived longitudinal strain of RV, performed by the same operator (intraobserver variability) or two independent operators (interobserver variability). All abbreviations are as shown in Figure 2.