Research Article

The Influence of Pin Deviation on the Fracture Correction and the Fixator Adjustment with Sensitivity and Kinematic Analysis

Xia Zhao and Jianfeng Li

Beijing University of Technology, Chaoyang District, Beijing 100124, China

Correspondence should be addressed to Jianfeng Li; lijianfeng@bjut.edu.cn

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Fracture correction is important orthopedics operation and can be performed by unilateral external fixator. Due to pin deviations being inevitable during the operation, searching the impacts of pin deviation on the fracture correction and fixator joint adjustment are important. This study puts forward evaluation index with sensitivity analysis for investigating the impact of three orientation deviations and three position deviations on fracture correction. Meanwhile, based on a clinical case from a 28-year-old female, the influence of pin deviation on the adjustment of fixator joints was analyzed by inverse kinematic method. Different pin deviations have different sensitivity; the sensitivity of orientation deviation is relatively larger than position deviation. The existence of pin deviation will result in the change of the adjustment value of fixator joints. In addition, the experiments of seven situations were established to verify the analytical results. This study revealed the sensitivity of different pin deviations which can also be used to predict the adjustment value of fixator joints and the accuracy of fracture correction. This research also helps to reduce operation time and decrease damage to soft tissue by reducing the frequency of inserting pins.

1. Introduction

Bone fracture is becoming a very prominent research topic mainly due to aging of population and traffic accident [1]. Fracture reduction is usually performed in orthopedics doctors to ensure that fractured bones were restored to their original location. It has been shown that fracture site using mechanical means through external fixators may have beneficial effects on bone healing and remodeling [2–4]. If fracture has not been accurately corrected, fracture mal-union or other fracture dislocation problems can lead to complications, such as early degenerative disease caused by abnormal joint contact pressures [5–7]. Complex types of malalignment often involve pediatric orthopaedic patients and they are often treated by osteotomy [8]. Regulating the rotational and translational joints of the fixator is usually necessary to reduce fracture and correct complex deformities [9, 10]. But the pins with different position deviations and orientation deviation will affect the accuracy of fracture correction. Clinically, the procedure of inserting pins into bone is usually performed artificially before an external fixator is applied for reduction. Under ideal situations, pins are inserted perpendicular to the bone and the fixator is applied in neutral or straight position [11]. However, in the actual situation, the existence of pin deviations is inevitable and it is difficult to insert the pins into the bone accurately and appropriately as ideal situation. Because the fixator has its own limitation, removing the attached fixator, redrilling new pin-holes, and then installing fixator on the new drilled pin-holes are sometimes necessary, but this kind of behavior will be harmful to bone tissue and extend the operation time [12]. If orthopedic surgeon knows how the pin deviation affects fracture correction and the fixator joint regulation rule, then they will be very skilled using external fixator. Meanwhile, if surgeons had more freedom to better arrange the pin-bone relationship and were not distracted to the subsequent reduction again, the quality of operation would be greatly improved.

To the author’s knowledge, although many prior studies discussed the sensitivities of two biomechanical methods
for fracture healing [13], the adjustability of two unilateral external fixators (Othofixx Dynamic Axial fixator and Dynafixs Standard Tibia fixator) for fracture reduction [14, 15] and the possibility of their nonaxial dynamization after fracture reduction [16], however, where pin deviation has the greatest impact on the accuracy of fracture reduction and the influence of pin deviations on the adjustment values of fixator joint, have been rarely investigated due to lack of a theoretical analysis.

So the aim of this study was, based on a clinical case, to discuss the effect of different pin deviations on fracture correction through sensitivity analysis method, through this study where pin deviation that has the greatest impact on fracture dislocation can be found. Secondly, how to adjust the fixator joints could help correct fracture completely when different pin deviations exist, which was also investigated through inverse kinematic analysis method where joints values can be directly obtained through analytic formulas. The establishment of the experiment also proves the correctness of the analytical results. This is of practical importance since from a physician's standpoint knowing how to accurately correct fracture dislocation is by understanding the relationship between the pin deviations and the adjustment of fixator joints, which can also help to provide theoretical guidance and improve the design of fixator.

2. Methods

2.1. Kinematic Model. A 6-degree-of-freedom (6-DOF) unilateral external fixator (Dyna-extor, Korean) was used in this study. In this study, only one bone pin at each bone segment is considered for rigid-body in kinematic analysis. This usage method has been reported in a previous article [17].

Taking proximal bone (B) as a reference, assuming that each bone pin has three Z1, Z2, Z3 axes, having three orientation deviations (φ1, φ2, φ3) and three position deviations (s1, s2, s3), which may exist in the process of inserting pins into bone, as shown in Figure 1. Detailed joint parameters of unilateral external fixator are shown in Table 1. The parameters of pin deviation for unilateral external fixator are shown in Table 2.

2.2. Establishment of Sensitivity Analysis Model. The precision of fracture reduction is affected by the position deviation and orientation deviation of pin. The effects of different pin deviations on the precision of fracture reduction are different. In order to find out which pin deviation has the greatest impact on the precision of fracture correction, the sensitivity analysis of pin deviation is needed, which describes the effect of degree of the small variation of pin deviations on the fracture correction [18].

The error calculation model of the fixator device can be established, which can be expressed explicitly.

\[ B = M(s_1, s_2, s_3, φ_1, φ_2, φ_3) \]  

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The transformation matrix from the proximal bone segment following formula can be obtained.

\[ A_M = A_{M_4}^4 M_5^5 M_6^7 M_8^9 M_{10}^{10} M_{12}^{12} M_B \]

(5)

Table 1: The joint parameters of unilateral external fixator.

| Joint variable | Kinematic pair | limit value of joints | Rotational axis |
|----------------|----------------|-----------------------|-----------------|
| a_5            | Distal revolute pair | 0–360 (degree) | Z_a            |
| a_6            | Distal revolute pair | 0–120 (degree) | Z_a            |
| d              | Moving pair         | 0–40 (mm)          | Z_a            |
| a_8            | Proximal revolute pair | 0–360 (degree) | Z_a            |
| a_9            | Proximal revolute pair | 0–120 (degree) | Z_a            |
| a_{10}         | Proximal revolute pair | 0–360 (degree) | Z_{10}         |

Table 2: The parameters of pin deviation for unilateral external fixator.

| Symbol of pin deviations | pin deviations | Error range of angle deviation | Angle deviation axis |
|--------------------------|----------------|------------------------------|---------------------|
| \( \varphi_1 \)          | Distal angle deviation | 0–20 (degree) | Z_1         |
| \( \varphi_2 \)          | Distal angle deviation | 0–20 (degree) | Z_2         |
| \( \varphi_3 \)          | Distal angle deviation | 0–20 (degree) | Z_3         |
| s_1                      | Distal position deviation | 0–10mm      | Z_1         |
| s_2                      | Distal position deviation | 0–10mm      | Z_2         |
| s_3                      | Distal position deviation | 0–10mm      | Z_3         |

Inverse kinematic analysis method was adopted to solve \( J \). In the mathematical analysis of the kinematic chain, \( A_M \) is the transformation matrix from the proximal bone segment to the distal bone segment which could be expressed as follows:

\[ A_M = A_{M_4}^4 M_5^5 M_6^7 M_8^9 M_{10}^{10} M_{12}^{12} M_B \]

(6)

Inverse kinematic analysis method was adopted to solve \( J \). Firstly, multiply \([12] M_B^{-1} [10] M_{12}^{-1} [9] M_{10}^{-1}\) on both right sides of (5) and obtain (6). \([12] M_B^{-1} [10] M_{12}^{-1} [9] M_{10}^{-1}\) are the inverse matrix of \([12] M_B\) \([10] M_{12}\) \([9] M_{10}\), respectively.

\[ H = A_{M_4}^4 M_5^5 M_6^7 M_8^9 M_9 \]

(7)
\[ M = A M_B \begin{bmatrix} [12 M_B]^{-1} & [10 M_{12}]^{-1} & [9 M_{10}]^{-1} \end{bmatrix} \]

\[ = \begin{bmatrix} M_{11} & M_{12} & M_{13} & M_{14} \\ M_{21} & M_{22} & M_{23} & M_{24} \\ M_{31} & M_{32} & M_{33} & M_{34} \\ M_{41} & M_{42} & M_{43} & M_{44} \end{bmatrix} \]  

(8)

Equation (7) denotes the transformation matrix from the coordinate system \( Z_A \) to \( Z_B \) in a counterclockwise direction; (8) refers to transformation matrix from the coordinate system of \( Z_A \) to \( Z_B \) in a clockwise direction in Figure 1(a). Given that the equations on both sides of (6) are equal, \( H \) and \( M \) are equal and first derivatives of \( H \) and \( M \) are equal, so (9)-(10) is derived.

\[ H_{14} = M_{14} \]
\[ H_{24} = M_{24} \]
\[ H_{34} = M_{34} \]  

(9)

According to (9), \( a_3, a_4, d \), can be solved. Detailed process can be shown in appendix.

\[ H'_{14} = M'_{14} \]
\[ H'_{24} = M'_{24} \]
\[ H'_{34} = M'_{34} \]  

(10)

According to (10), (11) can be obtained as follows:

\[ A_1 \phi_1' + A_2 \phi_2' + A_3 \phi_3' + A_4 s_1' - A_5 s_2' = B_1 \phi_1' + B_2 \phi_2' + B_3 \phi_3' + B_4 s_1' + B_5 s_2' \]
\[ = B_6 \phi_1' + B_7 \phi_2' + B_8 \phi_3' + B_9 s_1' + B_{10} s_2' \]  

(11)

According to (11), (12) can be obtained as follows:

\[ A_1 \phi_1' + A_2 \phi_2' + A_3 \phi_3' + A_4 s_1' - A_5 s_2' = B_1 \phi_1' + B_2 \phi_2' + B_3 \phi_3' + B_4 s_1' + B_5 s_2' \]
\[ = B_6 \phi_1' + B_7 \phi_2' + B_8 \phi_3' + B_9 s_1' + B_{10} s_2' \]
\[ s_1' - C_1 \phi_1' + C_2 \phi_3' - C_3 s_3' = C_4 \phi_1' - C_5 \phi_2' + C_6 \phi_3' + C_7 s_1' + C_8 s_3' \]
\[ = C_9 \phi_1' - C_{10} \phi_3' + C_{11} \phi_3' + C_{12} s_1' + C_{13} s_3' \]

Multiplying both sides of (5) by \([14 M_B]^{-1} [10 M_{14}]^{-1} [9 M_{10}]^{-1} [8 M_9]^{-1} [7 M_7]^{-1} [6 M_6]^{-1} (12)\) can be obtained as follows.

\[ A M_4 \cdot M_5 \cdot M_6 = A M_B \begin{bmatrix} [14 M_B]^{-1} & [10 M_{14}]^{-1} & [9 M_{10}]^{-1} & [8 M_9]^{-1} \end{bmatrix} \]
\[ K = A M_B \begin{bmatrix} [14 M_B]^{-1} & [10 M_{14}]^{-1} & [9 M_{10}]^{-1} & [8 M_9]^{-1} \end{bmatrix} \]

(14)

\[ P \text{ denotes the transformation matrix from } Z_A \text{ to } Z_B \text{ in a counterclockwise direction; } K \text{ refers to the transformation matrix from } Z_A \text{ to } Z_B \text{ in a clockwise direction, as shown in Figure 1(a). } P \text{ and } K \text{ are equal; thus, first derivatives of } K \text{ and } P \text{ are also equal, so (14) is derived.} \]

\[ K_{14} = P_{14} \]
\[ K_{24} = P_{24} \]
\[ K_{34} = P_{34} \]
\[ K_{13} = P_{13} \]  

(15)

According to (15), \( a_6, a_9, a_{10} \) can be solved. Detailed process can be expressed in appendix.

\[ K'_{14} = P'_{14} \]
\[ K'_{24} = P'_{24} \]
\[ K'_{34} = P'_{34} \]  

(16)

According to (16), (17) can be obtained as follows:

\[ D_1 B \phi_1' + D_2 B \phi_2' + B s_1' + D_3 B s_3' \]
\[ = D_4 \phi_1' + D_5 \phi_2' + D_6 s_1' + D_7 s_2' \]
\[ E_1 B \phi_1' + E_2 B \phi_2' + E_3 B s_1' + E_4 B s_2' - E_5 B s_3' \]
\[ = E_6 \phi_1' - E_7 \phi_2' + E_8 \phi_3' + E_9 s_1' + E_{10} s_2' \]
\[ F_1 B \phi_1' - F_2 B \phi_2' + F_3 B s_1' + F_4 B s_2' + F_5 B s_3' \]
\[ = F_6 \phi_1' + F_7 \phi_2' + F_8 \phi_3' + F_9 s_1' - F_{10} s_2' \]

(17)

According to (11) and (17), (18) can be obtained as follows:

\[ \begin{bmatrix} A_1 & A_2 & A_3 & 0 & -A_5 & A_4 \\ B_1 & B_2 & B_3 & 0 & B_4 & B_5 \\ 0 & -C_1 & C_2 & 1 & 0 & -C_3 \\ D_4 & D_5 & D_6 & 0 & -D_7 & D_8 \\ E_6 & -E_7 & E_8 & 0 & E_9 & E_{10} \\ 0 & F_6 & F_7 & 1 & 0 & -F_8 \end{bmatrix} \begin{bmatrix} \phi_1 \\ \phi_2 \\ \phi_3 \\ s_1 \\ s_2 \\ s_3 \end{bmatrix} \]

(18)
According to (18), (19) can be obtained as follows:

\[
\begin{bmatrix}
0 & A_7 & -A_8 & 1 & 0 & A_6 \\
B_6 & B_7 & B_8 & 0 & B_9 & -B_{10} \\
C_4 & -C_5 & C_6 & 0 & C_7 & C_8 \\
0 & D_1 & D_2 & 1 & 0 & D_3 \\
E_1 & E_2 & E_3 & 0 & E_4 & E_5 \\
F_1 & -F_2 & F_3 & 0 & F_4 & F_5
\end{bmatrix}^{-1}
\begin{bmatrix}
\varphi_1 \\
\varphi_2 \\
\varphi_3 \\
s_1 \\
s_2 \\
s_3
\end{bmatrix}
\cdot
\begin{bmatrix}
A_1 & A_2 & A_3 & 0 & -A_5 & A_4 \\
B_1 & B_2 & B_3 & 0 & B_4 & B_5 \\
0 & -C_1 & C_2 & 1 & 0 & -C_3 \\
D_4 & D_5 & D_6 & 0 & -D_7 & D_8 \\
E_6 & -E_7 & E_8 & 0 & E_9 & E_{10} \\
0 & F_6 & F_7 & 1 & 0 & -F_8
\end{bmatrix}
\tag{19}
\]

The detailed solution process and concrete expressions of \( A_1 \sim A_8, B_1 \sim B_{10}, C_1 \sim C_8, D_1 \sim D_8, E_1 \sim E_{10}, F_1 \sim F_8 \) in (11) and (17)–(20) can be explained in the appendix.

### 2.3. Sensitivity Evaluation Index of Pin Deviation

The influence degree of pin deviation on the fracture correction can be expressed by the error sensitivity coefficient. The corresponding amount of various types of deviation of pins is shown in Table 3.

In (21), \( q_s \) is displacement deviation at the fracture site; \( q_\varphi \) is angular misalignment at the fracture site shown as Figure 2. \( J_s \) is error transfer matrix of position deviation of pin; \( J_\varphi \) is error transfer matrix of orientation deviation of pin.

\[
q_s = J_s \delta s
\tag{21}
\]

\[
q_\varphi = J_\varphi \delta_\varphi
\]

According to (21), using Lagrange operator to establish Lagrange equation,

\[
L_s = \delta_s^T J_s^T J_s \delta s - \lambda_s (\delta_s^T \delta s - 1)
\tag{22}
\]

\[
L_\varphi = \delta_\varphi^T J_\varphi^T J_\varphi \delta_\varphi - \lambda_\varphi (\delta_\varphi^T \delta_\varphi - 1)
\]

In (22), \( \lambda_s \) and \( \lambda_\varphi \) are Lagrange multipliers. According to (22), construct the extreme value of Lagrange conditional equation:

\[
\frac{\partial L_s}{\partial \delta s} = 0 : J_s^T J_s \delta s - \lambda s \delta s = 0
\tag{23}
\]

\[
\frac{\partial L_\varphi}{\partial \delta_\varphi} = 0 : J_\varphi^T J_\varphi \delta_\varphi - \lambda_\varphi \delta_\varphi = 0
\]

In (23), Lagrange multipliers of \( \lambda_s \) and \( \lambda_\varphi \) are the eigenvalues of \( J_s^T J_s \) and \( J_\varphi^T J_\varphi \), respectively. The square of displacement deviation \( q_s \) and angular misalignment \( q_\varphi \) are shown as follows:

\[
\|q_s\|^2 = \Delta q_s^T \Delta q_s = \delta_s^T J_s^T J_s \delta_s = \delta_s^T \lambda_s \delta_s = \lambda_s
\tag{24}
\]

\[
\|q_\varphi\|^2 = \Delta q_\varphi^T \Delta q_\varphi = \delta_\varphi^T J_\varphi^T J_\varphi \delta_\varphi = \delta_\varphi^T \lambda_\varphi \delta_\varphi = \lambda_\varphi
\]

The extreme values of \( \Delta \delta s \) and \( \Delta \delta_\varphi \) are the root of \( \lambda_s \) and \( \lambda_\varphi \), respectively:

\[
\|q_s\| = \sqrt{\lambda_s} = \sqrt{\|J_s\|^2}
\tag{25}
\]

\[
\|q_\varphi\| = \sqrt{\lambda_\varphi} = \sqrt{\|J_\varphi\|^2}
\]
ΔBST and ΔBϕ have three extreme components, respectively, which can be written as follows:

\[
\begin{align*}
    f_{s1} &= \sqrt{\lambda_{s1}} = \sqrt{J_{T_{s1}}^{T_{s1}}} \\
    f_{s2} &= \sqrt{\lambda_{s2}} = \sqrt{J_{T_{s2}}^{T_{s2}}} \\
    f_{s3} &= \sqrt{\lambda_{s3}} = \sqrt{J_{T_{s3}}^{T_{s3}}} \\
\end{align*}
\]

In (26), λs1, λs2, and λs3 are the sensitivity coefficient of displacement dislocation ΔBS at the fracture site in XA, YA, ZA, three directions, respectively, caused by position deviation of pin.

\[
\begin{align*}
    f_{\varphi1} &= \sqrt{\lambda_{\varphi1}} = \sqrt{J_{T_{\varphi1}}^{T_{\varphi1}}} \\
    f_{\varphi2} &= \sqrt{\lambda_{\varphi2}} = \sqrt{J_{T_{\varphi2}}^{T_{\varphi2}}} \\
    f_{\varphi3} &= \sqrt{\lambda_{\varphi3}} = \sqrt{J_{T_{\varphi3}}^{T_{\varphi3}}} \\
\end{align*}
\]

In (27), λϕ1, λϕ2, and λϕ3 are the sensitivity coefficient of angular misalignment ΔBϕ at the fracture site in three directions of XA, YA, ZA, respectively, which caused orientation deviation of pin.

Take λs and λϕ as sensitivity evaluation index to assess the impact of position deviation of pin and orientation deviation of pin on the displacement dislocation and angular dislocation, respectively.

2.4. Clinical Application. In order to better study the effect of pin deviation on fixator joint adjustment and verify the sensitivity of pin deviation, a case was used.

In clinical practice, 28-year-old female was injured in a road traffic accident and treated with a unilateral external fixator. A 28-year-old female motorcyclist was brought into hospital after having been hit by a car from her right side. She had no medical history, took no regular medication, and had no allergies. The patient provided written informed consent for publication. The case has AP radiograph showing tibia deformity of 20° internal rotation and 20° external rotation and has 15° angular deformity and 5mm displacement deviations in three planes. By adjusting the fixator joints of a6, a6, a10, a9, and a8 with -6°, 20.8°, 9.3mm, -10.6°, -3.3°, and -12° respectively, the fracture deformity can be completely corrected.

Follow-up continued for a mean of 18 months (10–37 months). On the second day after surgery all patients had radiographs (anteroposterior, lateral, and mortise views) (Figure 2(a)). Partial weight bearing was allowed six weeks postoperatively and was gradually increased according to clinical and radiological evidence of union up to full weight bearing after complete union (Figure 2(b)) at a mean of 12 weeks (10–16 weeks). X-ray examination was repeated every month for a period of six months to evaluate bone union and fracture consolidation. Removal of the unilateral fixator was done for all cases after complete union at a mean period of 14 weeks (12–17 weeks). Removal of the fixator was followed by muscle strengthening exercises and physiotherapy.

3. Results

In this section, we discuss the sensitivities of different pin deviations. Meanwhile, based on a clinical case, the effect of pin deviation on fracture correction is also analyzed, which can verify the sensitivity of pin deviation from an analytical point of view. Moreover, the experiment was also established to verify the analytic results.

3.1. Simulation Results of Pin Deviations Sensitivity

3.1.1. Results of Sensitivity Analysis for Single Pin Deviation. We first investigate the sensitivity of single pin deviation in the appropriate range. The bigger the sensitivity is, the greater the effect of the pin deviation on the precision of the fracture reduction is.
ity is least impact on fracturedislocation of Bs
tation deviations; it can be noted that
 Bs
tos
deviations present an increasing trend; this indicates that the
completely. More joints with more amount to ensure fracture correction
the position deviation and which may be needed to adjust
greater impact on the accuracy of fracture correction than
deviation, which imply that the orientation deviation has a
likely to occur than displacement dislocation caused by pin
these sensitivity resultsshow that angulardislocation is more
two kindsof pin deviations simultaneously, as well as predict
the change of the fixator’s regulation. In Figure 4(a), the
sensitivity peak is 0.6986 at $\phi_1=20^\circ$, $\phi_2=20^\circ$; from Figures 4(b) and 4(c), the maximum sensitivity is 0.7618 and 0.6103;
they appear in ($\phi_1=20^\circ$ $\phi_2=20^\circ$) and ($\phi_1=20^\circ$ $\phi_3=20^\circ$), respectively. By comparing these three values, it is revealed that the
sensitivity of $\phi_2$ is greater than $\phi_3$ and $\phi_1$, because due to existing pin deviation of $\phi_2$, the sensitivity values of 0.6986 and 0.7618 are bigger than 0.6103. Meanwhile, under the
condition of having $\phi_2$, the value of 0.7618 is bigger than
0.6986, indicating the sensitivity of $\phi_2$ is higher than that of $\phi_1$. Besides, from Figure 4(a), the higher sensitivity of
0.612 also appears in the ($\phi_3=20^\circ$ $\phi_1=0^\circ$); this illustrates again
$\phi_3$ has a greater influence on fracture correction than
$\phi_1$, because the larger deviation sensitivity tends to occur
to the side of $\phi_2$. For Figure 4(b), the bigger sensitivity is
at ($\phi_3=0^\circ$ $\phi_5=20^\circ$), which is 0.7618, and for Figure 4(c) the
bigger sensitivity that is 0.561 appears at ($\phi_3=20^\circ$ $\phi_1=0^\circ$).
These results also illustrated that $\phi_2$ has larger impact than
$\phi_3$ and $\phi_1$ for fracture dislocation. $\phi_3$ has a greater influence
on fracture deformity correction than $\phi_1$.

For Figures 4(d), 4(e), and 4(f), the maximum sensitivity
values exist in $s_1=10$mm, $s_2=10$mm; $s_3=10$mm, $s_4=10$mm;
$s_5=10$mm, $s_6=10$mm; and they are 0.45437, 0.6371, and
0.59342, respectively. By comparing these three values, the
conclusions same as Figure 3(b) can be obtained as follows:
the sensitivity of $s_3$, $s_4$, and $s_1$ shows a gradual increasing
trend. In Figure 4(d), the higher sensitive value appears at the
$s_2=0$mm, $s_3=10$mm, and $s_1=0$mm, $s_2=10$mm; they are 0.38 and
0.4218, respectively. Obviously, the impact of $s_2$ on fracture
displacement correction is greater than $s_1$. For Figures 4(e) and 4(f), the higher sensitivity values exist at ($s_3=10$mm
$s_2=0$mm) and ($s_1=0$mm $s_3=10$mm); they all incline the side of
$s_3$; this indicates that the sensitivity of $s_3$ is bigger than $s_1$ and
$s_2$.

So we can put forward a hypothesis; as long as we know
the maximum sensitivity of single deviation, the maximum

Figure 3(a) shows sensitivity curves of three single orien-
tation deviations; it can be noted that $\phi_3$ has the largest sen-
sitivity when compared with $\phi_1$ and $\phi_2$. Besides $\phi_2$ and $\phi_3$, in
the entire range of pin deviations, the sensitivity was relatively
larger than $\phi_1$. This indicates that residual fracture deformity
of $B_P_2$ is most likely to appear. The possibility of fracture deformity of $B_P_1$ caused by $\phi_1$ is minimal. Meanwhile, with
the increase of the pin deviation, the sensitivity of all pin
deviations present an increasing trend; this indicates that the
increase in pin deviation may lead to increased sensitivity for
fracture dislocations.

From Figure 3(b), it can be seen that the sensitivity of $s_3$ is
higher than that of $s_1$ and $s_2$. With the increase of the position
deviation, the sensitivity also displays an increasing trend.

The sensitivity of $s_1$ is minimal, meaning that it has the
least impact on fracture displacement dislocation of $B_s$, and
$B_s$ has the biggest influence in displacement dislocation due
to $s_3$ having the biggest sensitivity compared with $s_2$ and $s_1$.

Comparing Figures 3(a) and 3(b), the maximum sensitivity
is $\phi_2$. Orientation deviation of $\phi_1$, $\phi_2$, and $\phi_3$ is relatively
larger than position deviation of $s_3$, $s_2$, and $s_1$, respectively.
These sensitivity results show that angular dislocation is more
likely to occur than displacement dislocation caused by pin
deviation, which imply that the orientation deviation has a
greater impact on the accuracy of fracture correction than
the position deviation and which may be needed to adjust
more joints with more amount to ensure fracture correction
completely.

In order to investigate whether the sensitivity of double
pin deviations has the same regularity, the following sensitivity
simulation was performed.

### 3.1.2. Results of Sensitivity Analysis for Double Deviations

The sensitivity results from Figure 4 help operation doctor
to seek the place of maximum sensitivity when there are
two kinds of pin deviations simultaneously, as well as predict

![Figure 3](image-url)
sensitivity of multiple deviations can be found. In order to verify this hypothesis, the following section analyzes the sensitivity of the multiple deviations of pin.

3.1.3. Results of Sensitivity Analysis for Multiple Deviations of Pin. For Figure 5, the volume of blue ball and red ball indicates the sensitivity of orientation deviation and position sensitivity, which have three different orientation deviations \( \varphi_1, \varphi_2, \varphi_3 \) and three different position deviations \( s_1, s_2, s_3 \) at the same time, respectively. With the increase of deviation, the volume of the ball increases gradually, so the sensitivity is also increased. For Figure 5(a), the growth rate of the spherical volume in the \( \varphi_2 \) direction is significantly larger than that in \( \varphi_1 \) and \( \varphi_3 \) directions. The change rate in the direction of \( \varphi_1 \) is the smallest. For Figure 5(b), the growth rate of the spherical volume in \( s_1 \) direction was relatively bigger than that in \( s_3 \) and \( s_1 \) directions. The change rate in the direction of \( s_1 \) is also the smallest as the same results in Figures 4(d)–4(f).

Comparing Figure 5(a) with Figure 5(b), the maximum position sensitivity appears in \( \varphi_1=20^\circ, \varphi_2=20^\circ, \varphi_3=20^\circ \) and \( s_1=10\text{mm}, s_2=10\text{mm}, s_3=10\text{mm} \), respectively; the results from this figure are consistent with previous assumptions since the maximum sensitivity also appears in the point which is also the maximum sensitivity in the single deviation.

Because the accuracy of fracture correction is guaranteed by adjusting fixator joints, it is necessary to investigate how to adjust fixator that can compensate fracture dislocations caused by pin deviation.

3.2. Results of the Effect of Pin Deviations on the Fixator Adjustment. Based on a clinical case in 2.4 (20° internal rotation, 20° external rotation and has 15° angular deformity, and 5mm displacement deviations on three planes).

The effect of pin deviations on the fixator adjustment was analyzed.

3.2.1. The Effect of Orientation Pin Deviation on Fixator Adjustment. Under the condition of ideal situation—having no pin deviation, \( a_8 \), \( d \) can be obtained by (9) and (15), they are -5.99\(^\circ\), 20.8024\(^\circ\), 9.3537mm, -10.5515\(^\circ\), -3.2705\(^\circ\), and -12.1301\(^\circ\), respectively. In the same way, when we have pin deviations, fixator joints also can be solved. Next we investigate the effect of pin deviation on fixator’s joints as follows.

Figure 6 displays the bar charts of the effect of different orientation deviation on the fixator joint adjustment \( (a_8, d) \). According to the results listed in Figures 6(a)–6(f), the results can be observed that the increase of orientation deviation of \( \varphi_1 \) will lead to rapid decrease of fixator joints of \( a_8 \). Since the regulating range of \( a_8 \) is only 36\(^\circ\), the existence of \( \varphi_1 \) can help \( a_8 \) avoid reaching the maximum value of regulation and expand the solution domain of the fixator.

It can be shown that the adjustment joint of \( a_8 \) is mainly affected by \( \varphi_2 \) and \( a_8 \) and \( a_{10} \) need to adjust greater quantity to ensure fracture correction accurately when compared with the condition of having no deviation, but this sharp increase in \( a_8 \) and \( a_{10} \) will result in fracture correction incompletely, because the adjustment range of the fixator is limited. On the contrary, the existence of \( \varphi_3 \) can make the maximum value decrease a lot; this will expand solution domain of \( d \).

Similarly, with the increase of \( \varphi_3 \), to ensure the fracture was corrected completely, the adjustment amount of \( a_8 \) needs to decrease greatly and \( a_8 \) will reduce a certain value, while \( \varphi_3 \) did not cause a lot of change to other joints compared with ideal situation.

The greater the sensitivity of pin deviation, the greater the adjustment amount of the fixator. According to the above
Figure 5: The sensitivity of multiple deviations of pin. (a) The sensitivity of multiple position deviations of pin. (b) The sensitivity of multiple orientation deviations of pin.

Figure 6: The influence of orientation deviation on the fixator joint adjustment. (a) The influence of orientation deviation on the adjustment of the fixator joint $a_5$. (b) The influence of orientation deviation on the adjustment of the fixator joint $a_6$. (c) The influence of orientation deviation on the adjustment of the fixator joint $d$. (d) The influence of orientation deviation on the adjustment of the fixator joint $a_8$. (e) The influence of orientation deviation on the adjustment of the fixator joint $a_9$. (f) The influence of orientation deviation on the adjustment of the fixator joint $a_{10}$. 
results that $\phi_2$ affects more joints with greater value than $\phi_3$ and $\phi_1$, it can be also proven that the sensitivity of $\phi_2$ is larger than $\phi_3$ and $\phi_1$; nevertheless the sensitivity of $\phi_1$ is minimal.

In addition to this, an important property was found in Figures 6(a)–6(f); when there are more deviations at the same time, the adjustment value of the joint is equal to the sum of the adjustment value of each deviation.

### 3.2.2. The Effect of Position Deviation of Pin on the Fixator Joint Adjustment

For Figures 7(a)–7(f), the effects of different position deviation on fixator adjustment are presented. As the sensitivity analysis above, there are more joints affected by $s_2$; with the increase of $s_2$, the joint regulation of $a_2$ increased significantly, $a_{10}$ declined with a rapid rate, but $a_d$ and $a_9$ show a slightly downward trend. The appearance of $s_2$ leads $a_2$ to reach the limit value in advance and also cause a great residual fracture dislocation and then will delay fracture healing.

When the deviation of $s_2$ increases, $a_d$ generated a higher regulatory value, $a_d$ and $d$ had lower value compared with ideal situation; the existence of $s_2$ also makes the fixator joint $a_d$ not capable enough to correct deformity which need greater regulation value.

The presence of the position deviation of $s_1$ makes $d$ increase significantly and also bring little increase in $a_d$ and little decrease in $a_9$. Similar to previous position sensitivity analysis, it is conceivable that $s_1$ has impact on more fixator joints with high value; the effect of $s_1$ on fixator joint is minimal. It also can be found that the influence of pin deviation on the fixator’s regulation has superposition characteristic, meaning that just knowing the influence of each pin deviation on adjustment amount of fixator joints and accordingly how to adjust fixator can also be predicted when there are many deviations; the adjustment value of fixator is the sum of adjustment value of every pin deviation.

### 3.3. Experimental Verification

The experiment of fixator-bone system for deformity correction at ideal situation shown in Figure 8 was established, in order to better verify the analytical results. In experiment, the bone deformation has $20^\circ$ internal rotation, $20^\circ$ external rotation, $15^\circ$ angular deformity, and $5$mm displacement deviations on three planes, which is the same as the clinical case. The adjustment values of fixator joints which need to correct deformity are also in accordance with clinical practice, meaning the experiment is reasonable. Moreover, seven situations were also established to verify the
analytical results; experimental results are shown in Table 4. The parameters of fixator-bone system in experiment are consistent with analytical model in Figure 1. In the process of experiment, one side of bone was fixed; by adjusting fixator joints, the deformity can be completely corrected. Table 4 shows the adjustment values of fixator joints at seven situations in experiment. Take the ideal situation as reference, when compared with pin deviations of $\varphi_2$ and $\varphi_3$, the adjustment value of the fixator joint of $a_4$ has the biggest discrepancy between the ideal situation and the existence of pin deviation $\varphi_1$. The presence of $\varphi_2$ causes a greater change than $\varphi_1$ and $\varphi_3$ in the amount of $a_5$, $a_8$, and $a_{10}$. Compared with $\varphi_1$ and $\varphi_2$, $\varphi_3$ has the biggest effect on $a_8$ and $a_9$. In summary, when compared with ideal situation, the existence of pin deviation will affect the regulating amount of fixator joint, and $\varphi_2$ will affect more joints and a greater amount of adjustment is needed; $\varphi_1$ has only bigger influences on one joint of $a_9$ and $\varphi_3$ causes bigger effect on two joints of $a_8$ and $a_9$. That also indicates that $\varphi_2$ has the bigger sensitivity than $\varphi_1$ and $\varphi_3$, meaning $\varphi_2$ has the biggest effect on the fixator joint adjustment. In addition, $\varphi_1$ has the minimum sensitivity compared to $\varphi_2$ and $\varphi_3$. These experimental results are consistent with analytical results for angular deviations.

For positional deviations, take the ideal situation with no pin deviations as a reference; compared with $s_3$ and $s_8$, the existence of $s_1$ makes a bigger change in fixator joint $d$. Meanwhile, $s_3$ has a great effect on $a_9$ and $a_4$. The existence of $s_5$ makes a great contribution to the bigger changes on $a_5$, $a_8$, and $a_{10}$ than $s_1$ and $s_2$. These results indicate that $s_1$ has the biggest sensitivity on the fixator joint adjustment and $s_1$ has minimum sensitivity, which can also verify the correctness of the analytical results. Table 5 shows the discrepancy between experiment results and analytical results for fixator joint adjustment value. The errors between experiment results and analytic results are very small and within twenty percent, meaning that the experimental results can verify the correctness of the analysis results.

4. Discussion

In this paper, the sensitivity analyses of pin deviation on fracture dislocation and the influence of pin deviation on fixator joint adjustment were presented; these researches provide important information and rules to doctor and researchers.

For sensitivity analysis, firstly, when there is only one kind of pin deviation, pin deviation having the maximum sensitivity can be found. Although $\varphi_1$, $\varphi_2$, $\varphi_3$ are all the orientation deviation and $s_1$, $s_2$, $s_3$ are all the position deviation, the sensitivity are not the same. According to the value of the maximum sensitivity, for orientation deviation, it can be judged that the sensitivity of $\varphi_2$ is greater than $\varphi_3$ and $\varphi_1$; the sensitivity of $\varphi_3$ is larger than that of $\varphi_1$. For position deviation, $s_2$ has the highest sensitivity and $s_1$ has the least sensitivity compared with $s_2$. Comparing orientation deviation with position deviation, the sensitivity of orientation deviation is relatively large. This phenomenon explained in previous study that angle deformation was difficult to correct which need to regulate more fixator joints [19]. Secondly, when there were many kinds of deviations, the location of the maximum sensitivity can be found by seeking the maximum sensitivity in single deviation. This discovery will reduce a lot time of computation, and as long as we know the position of the maximum sensitivity of the single deviation, the location of maximum sensitivity can also be found for the multiple deviations.

Based on clinical case, the effects of pin deviation on fixator joint are also investigated. Firstly, for orientation deviation, $\varphi_1$ have a great influence on fixator joint for $a_4$. Figure 8: The experiment of fixator-bone system for bone deformity at ideal situation. (a) The experiment of fixator-bone system before deformity correction. (b) The experiment of fixator-bone system after deformity correction.
\[\phi_2 \text{ have a great influence on } a_3, d, \text{ and } a_{10}. \phi_1 \text{ have a great influence on } a_5 \text{ and } a_9. \] Through the comparison, the impact of \(\phi_1, \phi_2, \text{ and } \phi_3\) on fixator joints, due to \(\phi_2\), affects more joints with more adjustment value and from this point of view, in which it can be drawn that \(\phi_2\) has the biggest influence on the adjustment of fixator; the effect of \(\phi_1\) is minimal. Meanwhile, for position deviation, \(s_3\) has a great influence on \(a_1, a_6, \) and \(a_{10}.\) Due to the existence of \(s_2\), the regulatory value of \(a_9\) and \(a_5\) changed a lot. \(s_1\) made a great change in \(d.\) Comparing \(s_2, s_1,\) and \(s_3, s_3\) can affect more joints, meaning when the deviation of \(s_3\) occurs, it is required to adjust more joints with greater amount of regulation in order to correct fracture completely; \(s_3\) has greater influence on the adjustment of fixator joint than \(s_2\) and \(s_3.\) The impact of \(s_1\) is minimal. The results of the effects of pin deviation on fixator joints verify the sensitivity analysis from a point of view. The greater the sensitivity of pin deviation, the more the joints affected. Another interesting finding is that the impact of pin deviation on fixator joints has the property of superposition; that is, if any deviations exist at the same time, that will have an impact on more fixator joints, which are equal to the sum of the effect of each deviation on fixator joint adjustment. Meanwhile, based on the clinical case, seven situations of pin deviation in experimental were set up to verify the analytic results. Moreover, in clinical practice, at the ideal situation, the adjustment values of fixator joints are consistent with analytical results and experimental results.

Through these analytic results from these findings, the orthopedist according to the actual situations reasonably increases or decreases the adjustment value of fixator joints, which could help correct the fracture residual dislocation caused by pin deviation; it also helps in reducing anesthesia time, lowering patient morbidity, and potentially lowering the risk of infection and radiation exposure, which also helps medical personnel to flexibly correct the fracture. The decrease of joint regulation due to the existence of pin deviation will increase the joint solution domain so as to expand the application scope of various bone deformities and avoid reaching the limit value of joints. Without knowing these information, complex reduction pattern could only be determined through trial and error, and pin needs to be inserted into bone more than once, which could prolong operation time and duplicate drilling attempts which may leave more bone tunnels that could potentially affect ligamentous reconstructions or complex fracture reduction [20].

The analysis technique and results reported herewith can provide useful information for the medical personnel who use external fixators in the management of long bone fractures and for device manufacturers to enhance their products’ efficacy in adjustability, modify their current fixators, or develop new devices. These results should also be considered for possible manual or motorized adjustment in the next generation of external fixator.

| Four situations | \(a_1\) (degree) | \(a_5\) (degree) | \(d\) (mm) | \(a_6\) (degree) | \(a_9\) (degree) | \(a_{10}\) (degree) |
|-----------------|------------------|------------------|------------|------------------|------------------|------------------|
| Ideal situation | -5.5             | 20               | 9          | -10              | -3               | -12              |
| \(\phi_1 = 20^\circ\) | 0.5              | 8.5              | 3          | 4                | -9.5             | -9               |
| \(\phi_2 = 20^\circ\) | 16               | 21               | -8         | -16.5            | -6.5             | -20.5            |
| \(\phi_3 = 20^\circ\) | 5.5              | -5               | 7.5        | -14              | 2.5              | -9.3             |
| \(s_1 = 10\) mm | -5               | 18.5             | 18.5       | -11.5            | -1.2             | -10.5            |
| \(s_2 = 10\) mm | -5.6             | 15               | 6.0        | -12              | 2                | -8.5             |
| \(s_3 = 10\) mm | -12              | 20               | 10.5       | -6.5             | -4.5             | -5               |

| Four situations | \(a_1\) (degree) | \(a_5\) (degree) | \(d\) (mm) | \(a_6\) (degree) | \(a_9\) (degree) | \(a_{10}\) (degree) |
|-----------------|------------------|------------------|------------|------------------|------------------|------------------|
| Ideal situation | 8%               | 3.8%             | 3.78%      | 5.2%             | 8.27%            | 1.05%            |
| \(\phi_1 = 20^\circ\) | 16%             | 2.96%            | 13.4%      | 7.69%            | 1.56%            | 1.26%            |
| \(\phi_2 = 20^\circ\) | 4.7%             | 0.213%           | 3.12%      | 1.17%            | 1%               | 1.7%             |
| \(\phi_3 = 20^\circ\) | 1.7%             | 1.82%            | 5.4%       | 3.05%            | 0.56%            | 19.19%           |
| \(s_1 = 10\) mm | 7.4%             | 2.32%            | 1.14%      | 5.41%            | 9.7%             | 0.52%            |
| \(s_2 = 10\) mm | 5%               | 1.51%            | 4.11%      | 9.33%            | 3.7%             | 5.357%           |
| \(s_3 = 10\) mm | 0.35%            | 2.43%            | 3%         | 19.19%           | 3.17%            | 0.85%            |
Appendix

First, according to (9), (A.1) can be solved as follows:

\[ \begin{align*}
    d_x a_1 \sin(a_6) + d_x n_{1x} \cos(a_5) \cos(a_6) \\
    + d_x a_{1x} \sin(a_5) \cos(a_6) &= E \\
    d_x a_{1y} \sin(a_6) + d_x n_{1y} \cos(a_5) \cos(a_6) \\
    + d_x a_{1y} \sin(a_5) \cos(a_6) &= F \\
    d_x a_{1z} \sin(a_6) + d_x n_{1z} \cos(a_5) \cos(a_6) \\
    + d_x a_{1z} \sin(a_5) \cos(a_6) &= G
\end{align*} \]  

(A.1)

According to (A.1), the fixator joint values—\( a_5, a_6, d \)—can be obtained by (A.2). Detailed solution process can be shown as follows:

\[ \begin{align*}
    a_5 &= 2\sin \left( \frac{2U_5}{(1 + U_5^2)} \right) \\
    a_6 &= 2\tan \left( \frac{-R_7 - \sqrt{(R_7)^2 + (R_8)^2}}{-R_8} \right) \\
    a_7 &= \frac{E}{(a_{1x} + n_{1x} J W + a_{1x} W)} \\
    d &= d_7 - D
\end{align*} \]  

(A.2)

Second, solving fixator joints of \( a_{10}, a_9, \text{and } a_8 \). According to (15), (A.3) can be obtained:

\[ \begin{align*}
    S_1 &= N_1 \sin(a_5) + N_2 \cos(a_5) \cos(a_{10}) \\
    &+ N_3 \cos(a_5) \sin(a_{10}) \\
    S_2 &= N_4 \sin(a_5) + N_5 \cos(a_5) \cos(a_{10}) \\
    &+ N_6 \cos(a_5) \sin(a_{10}) \\
    S_3 &= N_7 \sin(a_5) + N_8 \cos(a_5) \cos(a_{10}) \\
    &+ N_9 \cos(a_5) \sin(a_{10})
\end{align*} \]  

(A.3)

According to (A.3), \( a_{10}, a_9, \text{and } a_8 \) can be obtained by

\[ \begin{align*}
    a_{10} &= 2\tan \left( -\frac{N_{17} + \sqrt{N_{17}^2 - N_{16} N_{18}}}{N_{16}} \right) \\
    a_9 &= 2\tan \left( -\frac{N_1 + \sqrt{N_1^2 + N_{19}^2 - N_{16} N_{18} - S_1^2}}{-N_{19} - S_1} \right) \\
    a_8 &= 2\tan \left( -\frac{Q_{12} + \sqrt{Q_{12}^2 + Q_{11}^2 - Q_{13}^2}}{Q_{11} + Q_{13}} \right)
\end{align*} \]  

(A.4)

In (10), (15), and (18), the detailed expression of \( A_1 \sim A_8, B_1 \sim B_{10}, C_1 \sim C_8, D_1 \sim D_8, E_1 \sim E_{10}, \text{and } F_1 \sim F_8 \) is shown as follows:

\[ \begin{align*}
    A_1 &= \cos(\varphi_2) (l_1 + s_3) (- \sin(\varphi_1)) - s_2 \cos(\varphi_1) \\
    &- l_2 \cos(\varphi_1) \sin(\varphi_3) \\
    &- \sin(\varphi_1) \cos(\varphi_2) \sin(\varphi_3) \\
    A_2 &= - \cos(\varphi_1) \sin(\varphi_2) (l_1 + s_3) \\
    &+ \cos(\varphi_1) \cos(\varphi_2) \cos(\varphi_3) \\
    A_3 &= -l_2 \sin(\varphi_1) \cos(\varphi_3) \\
    &- \cos(\varphi_1) \sin(\varphi_3) \sin(\varphi_2) \\
    A_4 &= \cos(\varphi_1) \cos(\varphi_2) \\
    A_5 &= \sin(\varphi_1) \\
    A_6 &= \sin(\varphi_2) \\
    A_7 &= B_5 \cos(\varphi_2) \cos(\varphi_3) (l_3 - l_5) \\
    &- l_4 \sin(D_3) \cos(\varphi_3) \\
    A_8 &= l_4 \cos(\varphi_2) \sin(\varphi_3) \\
    B_1 &= -l_2 \sin(\varphi_1) \sin(\varphi_3) \\
    &- l_2 \cos(\varphi_2) \cos(\varphi_3) \sin(\varphi_1) \\
    &+ \cos(\varphi_1) \sin(\varphi_2) (l_1 + s_3) \\
    B_2 &= -l_2 \sin(\varphi_1) \cos(\varphi_2) \cos(\varphi_3) \\
    &- (l_1 + s_3) \sin(\varphi_1) \sin(\varphi_2) \\
    B_3 &= l_2 \cos(\varphi_1) \cos(\varphi_3) \\
    &+ l_2 \sin(\varphi_1) \sin(\varphi_3) \sin(\varphi_2) \\
    B_4 &= \cos(\varphi_1) \cos(\varphi_2) \\
    B_5 &= \cos(\varphi_2) \sin(\varphi_1) \\
    B_6 &= -l_4 \sin(\varphi_1) \sin(\varphi_2) \\
    &+ l_4 \cos(\varphi_2) \cos(\varphi_1) \sin(\varphi_3) \\
    &- B_5 \sin(\varphi_1) - B_6 \cos(\varphi_2) \cos(\varphi_1) \\
    &- \cos(\varphi_2) \cos(\varphi_1) (l_3 - l_5) \text{;}
\end{align*} \]
\[
\begin{align*}
\mathbf{B}_7 &= l_4 \cos(q\varphi_3) \sin(q\varphi_1) \cos(q\varphi_2) \\
&+ B_{53} \sin(q\varphi_1) \sin(q\varphi_2) \\
&+ \sin(q\varphi_2) \sin(q\varphi_3) (l_5 - l_3); \\
\mathbf{B}_8 &= l_4 \cos(q\varphi_3) \cos(q\varphi_1) \\
&- l_4 \sin(q\varphi_3) \sin(q\varphi_1) \sin(q\varphi_2); \\
\mathbf{B}_{10} &= \cos(q\varphi_1) \cos(q\varphi_2); \\
\mathbf{C}_1 &= \cos(q\varphi_1) (l_1 + s_3) - l_3 \sin(q\varphi_2) \cos(q\varphi_3); \\
\mathbf{C}_2 &= l_2 \cos(q\varphi_2) \sin(q\varphi_3); \\
\mathbf{C}_3 &= \sin(q\varphi_2); \\
\mathbf{C}_4 &= l_4 \cos(q\varphi_3) \sin(q\varphi_1) \\
&+ l_4 \sin(q\varphi_1) \cos(q\varphi_3) \sin(q\varphi_2) \\
&+ B_{52} \cos(q\varphi_1) - B_{53} \sin(q\varphi_1) \cos(q\varphi_2) \\
&- \sin(q\varphi_3) \cos(q\varphi_2) (l_5 - l_3); \\
\mathbf{C}_5 &= l_4 \cos(q\varphi_3) \cos(q\varphi_2) \\
&+ B_{53} \cos(q\varphi_1) \sin(q\varphi_3) \\
&+ \cos(q\varphi_1) \sin(q\varphi_2) (l_5 - l_3); \\
\mathbf{C}_6 &= l_4 \sin(q\varphi_3) \cos(q\varphi_1) \\
&+ l_4 \cos(q\varphi_3) \sin(q\varphi_3) \sin(q\varphi_2); \\
\mathbf{C}_7 &= \sin(q\varphi_1); \\
\mathbf{C}_8 &= \cos(q\varphi_1) \cos(q\varphi_2); \\
\mathbf{D}_1 &= B_{53} \cos(q\varphi_2) + \cos(q\varphi_3) (l_5 - l_3) \\
&- l_4 \sin(q\varphi_2) \cos(q\varphi_3); \\
\mathbf{D}_2 &= -l_4 \cos(q\varphi_2) \sin(q\varphi_3); \\
\mathbf{D}_3 &= \sin(q\varphi_2); \\
\mathbf{D}_4 &= -\sin(q\varphi_1) \cos(q\varphi_2) (l_1 + s_3) - s_2 \cos(q\varphi_1) \\
&- l_2 \cos(q\varphi_1) \sin(q\varphi_3); \\
\mathbf{D}_5 &= -\sin(q\varphi_2) \cos(q\varphi_1) (l_1 + s_3) \\
&- l_3 \cos(q\varphi_1) \cos(q\varphi_3) \sin(q\varphi_2) \\
&- d_5 \cos(a_5) \sin(q\varphi_1) \cos(q\varphi_3); \\
&+ d_5 \sin(a_5) \cos(q\varphi_1) \sin(q\varphi_3); \\
&- d_5 \cos(q\varphi_1) \sin(q\varphi_3) \cos(q\varphi_3); \\
\mathbf{D}_6 &= -l_2 \sin(q\varphi_1) \cos(q\varphi_3) \\
&+ d_5 \sin(a_5) \sin(q\varphi_1) \sin(q\varphi_3); \\
&+ l_3 \cos(q\varphi_1) \sin(q\varphi_3) \cos(q\varphi_3) \\
&- d_5 \cos(q\varphi_1) \sin(q\varphi_3) \cos(q\varphi_3); \\
&+ d_5 \sin(a_5) \cos(q\varphi_1) \sin(q\varphi_3); \\
&+ d_5 \cos(q\varphi_1) \sin(q\varphi_3) \cos(q\varphi_3); \\
\mathbf{E}_1 &= -l_4 \sin(q\varphi_1) \sin(q\varphi_3) \\
&+ l_4 \cos(q\varphi_3) \cos(q\varphi_1) \sin(q\varphi_2); \\
&- B_{52} \sin(q\varphi_1) - B_{53} \cos(q\varphi_2) \cos(q\varphi_1) \\
&- \cos(q\varphi_2) \cos(q\varphi_1) (l_5 - l_3); \\
\mathbf{E}_2 &= l_4 \cos(q\varphi_3) \sin(q\varphi_1) \cos(q\varphi_2) \\
&+ B_{53} \sin(q\varphi_2) \sin(q\varphi_1) \\
&+ \sin(q\varphi_2) \sin(q\varphi_1) (l_5 - l_3); \\
\mathbf{E}_3 &= l_4 \cos(q\varphi_3) \cos(q\varphi_1) \\
&- l_4 \sin(q\varphi_2) \sin(q\varphi_1) \sin(q\varphi_3); \\
\mathbf{E}_4 &= \cos(q\varphi_1); \\
\end{align*}
\]
$E_5 = \cos(q_2 \phi_1) \sin(q_1 \phi_1)$;

$E_6 = -s_2 \sin(\phi_1) + l_1 \cos(\phi_2) \cos(\phi_1)$
+ $l_2 \sin(\phi_1) \sin(\phi_2) + s_2 \cos(\phi_2) \cos(\phi_1)$
+ $d_7 \sin(\phi_6) \cos(\phi_1) \cos(\phi_3)$
+ $l_3 \cos(\phi_3) \cos(\phi_1) \sin(\phi_2)$
+ $d_7 \cos(\phi_6) \cos(\phi_2) \sin(\phi_3)$
+ $d_7 \sin(\phi_6) \cos(\phi_1) \sin(\phi_2) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \cos(\phi_2) \sin(\phi_1) \sin(\phi_2) \cos(\phi_3)$;

$E_7 = l_1 \sin(\phi_2) \sin(\phi_1) + s_3 \sin(\phi_2) \sin(\phi_1)$
+ $l_2 \cos(\phi_2) \cos(\phi_1) \sin(\phi_1)$
+ $d_7 \cos(\phi_6) \sin(\phi_2) \sin(\phi_1)$
+ $d_7 \cos(\phi_6) \cos(\phi_2) \sin(\phi_1) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \cos(\phi_2) \sin(\phi_1) \sin(\phi_2) \cos(\phi_3)$;

$E_8 = l_3 \cos(\phi_1) \cos(\phi_3)$
+ $d_7 \sin(\phi_6) \cos(\phi_2) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \sin(\phi_2) \sin(\phi_3)$
+ $l_3 \cos(\phi_3) \cos(\phi_3) \sin(\phi_3)$
+ $d_7 \sin(\phi_6) \cos(\phi_1) \cos(\phi_3) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \cos(\phi_1) \cos(\phi_3) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \cos(\phi_1) \cos(\phi_3) \sin(\phi_2) \sin(\phi_3)$
+ $d_7 \cos(\phi_6) \cos(\phi_1) \cos(\phi_3) \sin(\phi_2) \cos(\phi_3)$;

$E_9 = \cos(\phi_1)$;

$E_{10} = \cos(\phi_2) \sin(\phi_1)$;

$F_1 = l_4 \cos(q_1 \phi_1) \sin(q_3 \phi_1)$
+ $l_4 \sin(q_1 \phi_1) \cos(q_3 \phi_1) \sin(q_2 \phi_1)$
+ $B_{s2} \cos(q_1 \phi_1) - B_{s3} \sin(q_1 \phi_1) \cos(q_2 \phi_1)$
+ $\sin(q_1 \phi_1) \cos(q_2 \phi_1) (l_3 - l_5)$;

$F_2 = l_4 \cos(q_1 \phi_1) \cos(q_3 \phi_1) \cos(q_2 \phi_1)$
+ $B_{s3} \cos(q_1 \phi_1) \sin(q_2 \phi_1)$
+ $\sin(q_2 \phi_1) \cos(q_1 \phi_1) (l_3 - l_5)$;

$F_3 = l_4 \sin(q_1 \phi_1) \cos(q_3 \phi_1)$
+ $l_4 \sin(q_2 \phi_1) \cos(q_3 \phi_1) \sin(q_3 \phi_2)$;

$F_4 = \sin(q_1 \phi_1)$;

$F_5 = \cos(q_1 \phi_1) \cos(q_2 \phi_1)$;

$F_6 = \cos(q_2 \phi_1) l_1 + s_2 \cos(q_2 \phi_2) - l_2 \sin(q_2 \phi_2) \cos(q_3 \phi_3)$
+ $d_7 \cos(a_6) \sin(a_6) \cos(q_2 \phi_2)$
+ $d_7 \sin(a_6) \sin(q_2 \phi_2) \sin(q_3 \phi_3)$
+ $d_7 \cos(a_6) \cos(a_6) \cos(q_3 \phi_3) \sin(q_2 \phi_2)$;

$F_7 = l_2 \cos(q_2 \phi_2) \sin(q_3 \phi_3)$
+ $d_7 \sin(a_6) \cos(q_2 \phi_2) \cos(q_3 \phi_3)$
+ $d_7 \cos(a_6) \cos(a_6) \cos(q_2 \phi_2) \sin(q_3 \phi_3)$;

$F_8 = \sin(q_2 \phi_2)$;

(A.5)

**Data Availability**

The data used in this study are analyzed and experimented by ourselves.

**Disclosure**

The data used in this study are analyzed and experimented by ourselves.

**Conflicts of Interest**

No conflicts of interest exits in the submission of this manuscript.

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