M2 cortex-dorsolateral striatum stimulation reverses motor symptoms and synaptic deficits in Huntington’s disease

Sara Fernández-García¹,²,³, Sara Conde-Berrioza³, Estíber García-García¹,²,³, Clara Gort-Paniello¹,²,³, David Bernal-Casas⁴, Gerardo García-Díaz Barriga¹,²,³, Javier López-Gil², Emma Muñoz-Moreno², Guadalupe Soria², Leticia Campa²,⁵,⁶, Francesc Artigas²,⁵,⁶, Manuel José Rodríguez¹,²,³, Jordi Alberch¹,²,³,⁷, Mercè Masana¹,²,³*

¹Departament de Biomedicina, Institut de Neurociències, Facultat de Medicina i Ciències de la Salut, Universitat de Barcelona, Barcelona, Spain; ²Institut d’Investigacions Biomèdiques August Pi i Sunyer (IDIBAPS), Barcelona, Spain; ³Centro de Investigación Biomédica en Red sobre Enfermedades Neurodegenerativas (CIBERNED), Madrid, Spain; ⁴Departament de Estadística, Facultat de Biologia, Universitat de Barcelona, Barcelona, Spain; ⁵Institut d’Investigacions biomèdiques de Barcelona (IIBB), Consejo Superior de Investigaciones Científicas (CSIC), Barcelona, Spain; ⁶Centro de Investigación Biomédica en Red sobre Enfermedades Mentales (CIBERSAM), Madrid, Spain; ⁷Production and Validation Center of Advanced Therapies (Creatio), Faculty of Medicine and Health Science, University of Barcelona, Barcelona, Spain

Abstract Huntington’s disease (HD) is a neurological disorder characterized by motor disturbances. HD pathology is most prominent in the striatum, the central hub of the basal ganglia. The cerebral cortex is the main striatal afferent, and progressive cortico-striatal disconnection characterizes HD. We mapped striatal network dysfunction in HD mice to ultimately modulate the activity of a specific cortico-striatal circuit to ameliorate motor symptoms and recover synaptic plasticity. Multimodal MRI in vivo indicates cortico-striatal and thalamo-striatal functional network deficits and reduced glutamate/glutamine ratio in the striatum of HD mice. Moreover, optogenetically-induced glutamate release from M2 cortex terminals in the dorsolateral striatum (DLS) was undetectable in HD mice and striatal neurons show blunted electrophysiological responses. Remarkably, repeated M2-DLS optogenetic stimulation normalized motor behavior in HD mice and evoked a sustained increase of synaptic plasticity. Overall, these results reveal that selective stimulation of the M2-DLS pathway can become an effective therapeutic strategy in HD.

Introduction Huntington’s disease (HD) is an inherited neurodegenerative disorder with symptomatic manifestations, including involuntary movements such as chorea, dystonia, poor motor coordination, psychiatric, and cognitive symptoms. HD is caused by a CAG repeat expansion in the huntingtin (Htt) gene that translates into a polyglutamine tract in the Htt protein. Mutant Htt (mHtt) is expressed throughout the brain and disrupts a wide range of molecular pathways and signaling cascades, yet HD pathology is most prominent in the basal ganglia circuitry.

The central hub of the basal ganglia is the striatum, which controls movements and behavior through a myriad of inputs and outputs (Calabresi et al., 2014; Freeze et al., 2013; Rothwell et al.,...
In HD, motor symptoms emerge from dysregulated information flow through the basal ganglia circuits. Disturbances of the cortico-striatal communication have a leading role in HD network dysfunction, with alterations appearing in prodromal HD (Burgold et al., 2019; Dumas et al., 2013; Unschuld et al., 2012). Specifically, the caudate nucleus and the premotor cortex are predominantly affected (Unschuld et al., 2012). In HD mouse models, there is abundant evidence of a progressive disconnection between cortex and striatum (Cepeda et al., 2007; Veldman and Yang, 2018). Cortico-striatal dysfunction in HD is strongly supported by the impaired cortico-striatal-dependent motor functions (Hong et al., 2012; Puigdellivol et al., 2015), altered paired-pulse facilitation at cortico-striatal synapses (Milnerwood and Raymond, 2007), reduction of striatal excitatory postsynaptic currents with loss of cortico-striatal synapses (Cepeda et al., 2003; Deng et al., 2013); and altered glutamate release in the striatum of transgenic R6/1 mice (Nicniciu et al., 2001). Moreover, reducing mHtt in the striatum is not sufficient to revert HD neurodegeneration, while reducing mHtt expression in both striatum and cortex ameliorates behavioral and neuropathological features of HD animals (Gu et al., 2005; Wang et al., 2014). Thus, a progressive disconnection of cortico-striatal pathways alters the information processing in basal ganglia circuitry, leading to motor disturbances. However, we do not know yet if specific cortico-striatal pathways are affected.

In this study, we aimed to further map cortico-striatal dysfunction in HD by using in vivo multimodal magnetic resonance imaging (MRI) techniques in the R6/1 HD mouse model. We took advantage of optogenetic tools (Zhang et al., 2010) and high-resolution cortico-striatal maps (Hintiryan et al., 2016) to modulate cortico-striatal function in HD mice. More specifically, we modulated the secondary motor (M2) cortex projection to dorsolateral striatum (DLS), whose structural alterations have been previously reported in HD (Hintiryan et al., 2016). Then, we used optogenetics coupled to in vivo microdialysis and to ex vivo multi-electrode arrays (MEAs) to characterize cortico-striatal dysfunction in symptomatic HD mice. With this knowledge, we aimed to test novel therapeutic interventions based on circuit restoration, an approach previously found successful for other basal ganglia disorders (Gradinaru et al., 2009; Kravitz et al., 2010).

Strikingly, selective optogenetic stimulation of the M2-DLS afferent pathway successfully rectified motor learning and coordination deficits in symptomatic HD mice. These effects were associated with improvements in synaptic plasticity such as induced long-term depression (LTD) and normalization of spine density within the striatum of HD mice. Our findings reveal that the function of the M2 cortex-DLS circuit is deeply impaired in the present HD mouse model, and indicate that selective stimulation of this pathway induces long-lasting plasticity effects that significantly ameliorate motor symptoms in HD.

Results

The striatum of HD mice shows decreased functional connectivity with afferent regions during rest

To evaluate distinct striatal circuit alterations in the transgenic R6/1 mouse model of HD, we studied the functional connectivity using resting-state fMRI (rs-fMRI) in ~20-week-old R6/1 mice. First, the analysis of the whole–brain network showed reduced strength (p = 0.037) and global efficiency (p = 0.029) in HD mice compared to WT mice, as assessed by the Student’s t-test. In a more specific manner, we evaluated functional connectivity using seed-based analysis between the striatum and selected brain regions involved in basal ganglia function (Figure 1; Supplementary files 1–2). We found that the striatum from the left hemisphere in HD mice showed a positive correlation with a smaller brain area (252 ± 77 mm$^3$) than the corresponding in WT mice (335 ± 17 mm$^3$; p = 0.00016, Student’s t-test). Then, to evaluate functional connectivity differences, we measured the mean correlation value for the regions of interest, automatically identified based on a mouse brain atlas, and analyzed genotype differences (Figure 1c). Two-way ANOVA showed a significant genotype effect
Glutamate neurotransmission is reduced in the striatum of symptomatic HD mice

To further characterize cortico-striatal function in HD, we measured brain metabolites in the striatum of ~17-week-old mice, using single-voxel $^1$H Magnetic Resonance Spectroscopy (MRS) (Figure 2). Two-way ANOVA showed metabolite-genotype interaction effect ($F_{(7,154)} = 17.49$; $p < 0.0001$) and Bonferroni post hoc analysis of the absolute metabolite concentrations revealed similar glutamate and glutamine, increased creatine+phosphocreatine (Cr+PCr; $p = 0.0013$), and decreased N-Acetyl-aspartate (NAA; $p = 0.0371$), NAA + NAA-Glutamate (NAAG; $p = 0.0057$) and Taurine ($p < 0.0001$; Figure 2b), in line with those previously described for the knock-in (KI) model of HD (Pépin et al.,...
Figure 2. Brain metabolites in the striatum are altered in symptomatic HD mice. (a) Representative $^1$H MRS signal from abundant metabolites in the striatum of WT (blue line) and HD (red line) mice. Voxel location in the striatum is illustrated in coronal (top panel) and sagittal brain view (bottom panel). (b) Metabolites concentration quantification (mmol/kg w.w.). (c) The glutamate/glutamine ratio was calculated as an indicator of glutamate neurotransmission. (d) Representative coronal images of GluCEST in WT (top) and HD mice (middle) and manually drawn ROIs used for quantification (bottom). (e) GluCEST quantification of striatum and cortex. Values were calculated as the GluCEST value (percentage of asymmetry at 3 ppm) versus minimum GluCEST value in the ventricles and left and right hemisphere values were averaged. Data are represented as mean ± SEM (WT n = 10 and HD n = 13 mice). Each gray point represents data from an individual mouse. *p < 0.05, **p < 0.01, ***p < 0.001 HD versus WT. Abbreviations: Glu: glutamate; Gln: glutamine; GSH: glutathione; NAA: N-Acetyl-aspartate; Tau: taurine; NAAG: N-Acetyl-aspartyl-glutamate; Ins+Glyc: inositol + glycine.

The online version of this article includes the following figure supplement(s) for figure 2:

Figure supplement 1. Correlation of glutamate levels obtained from GluCEST and $^1$H MRS in the striatum.
Moreover, the glutamate/glutamine ratio, which is related to glutamate released as a neurotransmitter, was reduced in HD mice (p = 0.0072, Student’s t-test), suggesting a reduced glutamatergic release in the striatum of HD mice (Figure 2c).

To study the relationship between cortical and striatal levels of glutamate, we also used chemical exchange saturation transfer (CEST) technique, which has been demonstrated to map glutamate levels (Cai et al., 2013; Cai et al., 2012) with higher sensitivity and spatial resolution compared to $^1$H MRS (Bagga et al., 2018; Pépin et al., 2016). GluCEST showed decreased glutamate levels in the striatum and cortex of HD mice compared to WT animals, as shown by two-way ANOVA brain region effect ($F_{(1,21)} = 16.59; p = 0.0005$), genotype effect ($F_{(1,21)} = 6.541; p = 0.0183$) but not region/genotype interaction effect ($F_{(1,21)} = 3.286; p = 0.0842$), and Bonferroni post hoc comparisons showed significant differences between WT and HD in both regions (Figure 2d–e). Moreover, a significant correlation between MRS and GluCEST was observed for all cases ($r = 0.5979; p = 0.0026$; Figure 2—figure supplement 1).

Selective M2 cortex-DLS optogenetic stimulation reveals deficient glutamate release in HD mice

To functionally assess cortico-striatal function in HD mice, we evaluated optogenetically-induced glutamate release in the striatum of WT and HD mice using in vivo microdialysis (Figure 3a–c). Among the different frontostriatal pathways, we chose to stimulate the projection from rostral M2 cortex to DLS based on the structural alterations previously reported in HD (Hintiryan et al., 2016). After six baseline dialysate samples (collected every 6 min), blue light was ON for 5 min (during sample seven collection), and six additional samples were collected in light-OFF conditions. Extracellular glutamate concentration under baseline conditions, calculated as the mean of the first six collected samples, was similar between genotypes (WT: 0.73 ± 0.08; HD: 0.69 ± 0.06 pmol/sample). Blue light stimulation led to increased glutamate levels in WT-ChR2, which returned to baseline levels after stimulation. However, increases in glutamate level were not detected in HD-ChR2 mice nor in the WT-YFP and HD-YFP control mice. Two-way ANOVA showed a significant effect of time ($F_{(12,144)} = 2.219; p = 0.0136$), and Bonferroni post hoc analyses showed significant differences between WT-ChR2 and all other groups during stimulation (sample 7, blue box; Figure 3b). These data indicate a reduced cortico-striatal-dependent glutamate release in symptomatic HD mice compared to WT controls.

Striatal neuronal response to M2 cortex afferent stimulation is dampened in HD mice

To test whether optical stimulation was effectively activating the M2 cortex-DLS pathway, we performed multi-electrode array (MEA) recordings in sagittal acute brain slices of WT-ChR2 and HD-ChR2 mice (Figure 3d–e). We recorded IPSC in the dorsal striatum after stimulation with increasing light intensities to create a normalized input-output assay. We found that optic stimulation of M2 cortex afferent pathways evoked IPSC in the dorsal striatum (Figure 3e). Two-way ANOVA showed that the amplitude of the evoked striatal IPSC was significantly larger in WT-ChR2 than in HD-ChR2 mouse (genotype effect; $F_{(10,55)} = 1.188; p = 0.0395$) followed by Bonferroni post hoc comparisons. Also, increasing laser intensity led to IPSC of larger amplitude in both mouse groups (light intensity factor; $F_{(10,55)} = 9.906; p < 0.00001$). These results confirm the reliability of our optogenetic approach as they provide evidence of a specific striatal response to the selective optogenetic activation of cortico-striatal afferents. Besides, the results further confirm that the M2 cortex-DLS circuit in HD is functionally altered, possibly due to both pre- and postsynaptic effects.

Repeated M2 cortex-DLS stimulation improves exploratory and stereotyped behavior in symptomatic HD mice

Next, we examined whether the increased glutamatergic input onto DLS - induced by optogenetic stimulation of M2 cortical afferents - translated into an improved motor behavior in HD mice. To this end, we performed repeated optogenetic cortico-striatal stimulation in freely moving mice in the open field (OF) apparatus (Figure 4). We placed the mice in the OF and, after 5 min (PRE-stimulation), we delivered blue light for 1 min, and we left the mice in the apparatus for 5 extra min (POST-stimulation). Light stimulation was delivered at 10 Hz, which is within the physiological range of cortical pyramidal neurons firing and a similar protocol has been used for repeated cortico-striatal
Figure 3. M2 cortex-dorsolateral striatum function is impaired in HD mice. (a) Schematic representation showing AAV-ChR2 and control AVV-YFP constructs and injection location at M2 cortex and fiber-optic cannula and microdialysis probe implants. (b) Dialysate samples were collected every 6 min and glutamate was subsequently measured. (c) WT ChR2: Glutamate levels were significantly reduced in HD ChR2 mice compared to WT ChR2 mice. (d) ePSC amplitude was significantly reduced in HD ChR2 mice compared to WT ChR2 mice. Figure 3 continued on next page.
Figure 3 continued

analyzed by HPLC. A 473 nm light stimulation was delivered at 10 Hz bilaterally for 5 min in freely moving mice during sample 7 (blue box). Glutamate level of each dialyse sample in the striatum is represented as a percentage of the mean glutamate baseline levels (samples 1–6; WT-YFP n = 3, WT-ChR2 n = 4, HD-YFP n = 4, HD-ChR2 n = 5 mice/group). (c) Histological images from one representative WT-ChR2 (top) and one HD-ChR2 (bottom) showing AAV expressed in M2-cortex (left), fiber-optic cannula in the DLS (center), and microdialysis probe just below the fiber-optic cannula (right). Arrows indicate the tip of the fiber-optic cannula and location of the microdialysis probe membrane, respectively. (d) Schematic representation of multi-electrode array recordings in slices and a representative image showing the electrodes and the location of light stimulation. AAV-ChR2 was injected at the M2 cortex. Sagittal slices were obtained for light-induced recording. A fiber-optic cannula was used to locate the light on top of the dorsolateral striatum. (e) The amplitude of light-intensity-induced striatal field post synaptic currents (IPSC) in WT and HD mice. Inset: Representative traces of the light-induced electrical response. Two-way ANOVA with Bonferroni post hoc comparisons test was performed. Values are expressed as mean ± SEM (WT-ChR2 n = 4, HD-ChR2 n = 3 mice). *p < 0.05.

Optogenetic stimulation (Ahmari et al., 2013). The distance traveled, rearing time, and stereotypies were recorded during the 11 min period (Figure 4b and d). We repeated the same procedure three times, each one-week apart, in symptomatic 20, 21, and 22 week-old-mice. The precision of the injection, evaluated by YFP expression, and location of fiber-optic cannula were assessed from histological slices (Figure 4c; Figure 4—figure supplement 1). While some of the neurons expressing YFP were located in M2 cortex, the presence of fluorescent fiber bundles and axons were found in cortical, striatal, and other subcortical projecting areas previously described (Hintiryan et al., 2016; Reiner et al., 2010; Shepherd, 2013). Fiber-optic cannulas were placed caudal in the dorsolateral striatum, avoiding direct activation of passing fibers expressing the AAV constructs.

The total distance traveled was similar in all experimental groups during OF sessions, and light stimulation did not induce significant changes in locomotor activity before, during, or after the light stimulation (Figure 4e, Figure 4—figure supplements 2a and 3a). Two-way ANOVA with group and session as factors was performed before and after optogenetic stimulation (Figure 4e). The distance traveled did not show significant interaction (F(6,104) = 0.4931; p = 0.8123), time (F(2,104) = 1.143; p = 0.3227) or group effects (F(3,104) = 1.415; p = 0.2425) during the 5 min PRE period, while showed group effects during 5 min POST stimulation (F(3,104) = 3.856; p = 0.0116) but not interaction (F(6,104) = 0.3272; p = 0.9214) or time (F(2,104) = 0.4005; p = 0.6710) effects. Bonferroni post hoc test failed to show significant main group effects, although there was a tendency for HD-ChR2 to increase the distance traveled compared to HD-YFP after stimulation.

By contrast, exploratory behavior, measured as rearing time, was reduced in HD mice compared to WT, as previously described for KI mice (Pépin et al., 2016). Optogenetic stimulation induced an increase of exploratory behavior over the sessions in HD-ChR2 mice (Figure 4f, Figure 4—figure supplements 2b and 3b). Two-way ANOVA with group and session as factors was performed before and after optogenetic stimulation (Figure 4f). The rearing time showed significant group effect (F(3,104) = 6.777; p = 0.0003) but not interaction (F(6,104) = 1.174; p = 0.3261) or time (F(2,104) = 1.199; p = 0.3057) effects during the 5 min PRE period; and showed group and time effects during 5 min POST stimulation (F(3,104) = 9.199; p < 0.0001) and (F(2,104) = 3.472; p = 0.0347, respectively) but not interaction (F(6,104) = 0.6651; p = 0.6780). Bonferroni’s main group comparison revealed that the HD-YFP group significantly showed reduced exploratory behavior compared to all other groups before stimulation, indicating that exploratory behavior in stimulated HD mice increased over the sessions and that the effects last for at least 1 week. Moreover, after the stimulation WT-ChR2 group showed reduced rearing time compared to WT-YFP, and it was no longer different from HD-YFP and HD-ChR2 groups, indicating an acute effect of the optogenetic stimulation in WT mice. Analysis of exploratory behavior during the 11 min period (Figure 4—figure supplements 2b and 3b) showed that exploratory behavior in HD mice is increased over the sessions, further indicating long-lasting effects of the optogenetic stimulation on rearing time.

Also, we measured stereotypic grooming in the same mice (Figure 4g, Figure 4—figure supplements 2c and 3c), as repetitive grooming is associated with stereotypic pathological behavior that may reflect cortico-striatal dysfunction. In non-stimulated conditions, HD mice showed an increased stereotypic behavior, as compared to WT mice, in line with the previously described increase in...
Figure 4. Repeated optogenetic stimulation of the cortico-striatal pathway recovers exploratory and stereotypic behavioral deficits in symptomatic HD mice. (a) Schematic diagram showing AAV-ChR2 and control AAV-YFP constructs injections at the M2 cortex and fiber-optic cannula implant in the DLS allowing light stimulation of cortically infected neuronal axons. (b) Locomotion (distance traveled), exploration time (rearing time), and stereotypic grooming (grooming time) were evaluated during 11 min open field session. Optogenetic stimulation consisted of 10 Hz light stimulation for 1 min
grooming in KI mice (Pépin et al., 2016). Interestingly, repeated optogenetic stimulation reduced stereotypical behavior in HD-ChR2 mice. Two-way ANOVA with group and session as factors showed significant group effect ($F_{(3,104)} = 5.073; p = 0.0026$) but not interaction ($F_{(6,104)} = 1.200; p = 0.3124$) or time ($F_{(2,104)} = 1.029; p = 0.3609$) effects during the 5 min PRE period; and also showed significant group effects ($F_{(3,104)} = 4.931; p = 0.003$) but not interaction ($F_{(6,104)} = 0.8105; p = 0.5641$) or time ($F_{(2,104)} = 1.315; p = 0.2729$) effects during the 5 min POST period. Bonferroni’s main group comparison revealed that the HD-YFP group significantly showed increased stereotypic grooming before and after stimulation. Moreover, analysis of stereotypic behavior during the whole 11 min period and for each min showed a significant reduction of stereotypic grooming during the last OF session (Figure 4—figure supplements 2c and 3c).

Overall, our data revealed that M2 cortex-DLS stimulation had a stronger impact on the modulation of spontaneous activity of HD mice, while acute locomotor activation was not observed. The effects of the light stimulation on exploratory behavior were manifested before and after stimulation over the sessions, suggesting some long-lasting effects evoked by the optogenetic stimulation of this M2-DLS circuit (Figure 4—figure supplement 3c).

Motor learning and coordination deficits in symptomatic HD mice are recovered by optogenetic stimulation of the M2-DLS cortico-striatal pathway

We further explored the effects of M2-DLS stimulation on motor learning and coordination. Motor learning was assessed by measuring the latency to fall from an accelerating rotarod. HD mice showed reduced latency to fall compared to WT, as previously described (Creus-Muncunill et al., 2019; Puigdellivol et al., 2015). Interestingly, optogenetic stimulation of the M2 cortex-DLS pathway increased the latency to fall from the rod in HD-ChR2 mice to similar levels as WT mice. Repeated measures ANOVA showed significant effects of mice group ($F_{(3,35)} = 6.058; p < 0.0020$), time ($F_{(11,385)} = 24.24; p < 0.0001$), and interaction ($F_{(33,385)} = 2.160; p < 0.0003$). Moreover, Bonferroni post hoc analyses showed significant differences only between WT-YFP and HD-YFP mice, which are mostly lost in HD-ChR2 (Figure 5c).

Besides, we evaluated motor balance and coordination by measuring the ability of mice to walk across a balance beam for 2 min (Figure 5d). The number of 5 cm-frames crossed was reduced in HD-YFP mice compared to WT mice, as already described (Creus-Muncunill et al., 2019). Remarkably, M2 cortex-DLS stimulation ameliorated motor coordination in HD-ChR2 mice, reaching similar levels to WT mice. Two-way ANOVA showed a genotype effect ($F_{(1,34)} = 7.226; p < 0.011$), with no stimulation ($F_{(1,34)} = 1.270; p = 0.267$) or interaction ($F_{(1,34)} = 2.863; p = 0.0998$) effects, and Bonferroni post hoc analyses showed significant differences only between WT-YFP and HD-YFP mice groups. These data suggest that the prior activation of the M2-DLS circuit induces long-lasting effects that impact the basal ganglia motor function. Moreover, our results indicate that by repeated activation of selected cortico-striatal circuits, that is, M2-DLS circuit, we can successfully ameliorate motor function in HD.
Repeated cortico-striatal stimulation triggers persistent improvements of synaptic plasticity in symptomatic HD mice

We explored whether these behavioral effects were due to the long-lasting synaptic re-wiring of the cortico-striatal circuit in HD (Figure 6). We repeated the M2-cortex-DLS stimulation procedure in vivo (Figure 6—figure supplement 1) and then explored if the repeated optogenetic stimulation modulates the electrophysiological response in cortico-striatal sagittal slices. On the 3rd stimulation week, we obtained cortico-striatal slices and recorded fPSC response to increasing light intensity stimulation. We found that increasing laser intensity led to striatal fPSC of increasing amplitude in both WT-ChR2 and HD-ChR2 groups as shown by two-way ANOVA light intensity effect ($F_{(7,154)} = 39.05; p < 0.0001$). Interestingly, we found no genotype effect or genotype/light intensity interaction ($F_{(7,154)} = 39.05; p < 0.0001$). Then, we recorded fPSC in the striatum after the electrical stimulation of cortical afferents. We induced LTD, which is known to be altered in HD mouse (Creus-Muncunill et al., 2019; Cummings et al., 2006; Ghiglieri et al., 2019; Li et al., 2015), using a theta-burst stimulation (TBS)
**Figure 6.** Repeated optogenetic cortico-striatal stimulation restores synaptic plasticity and dendritic spine density in HD mice. (a) Surgery, behavior, and optogenetic experimental timeline. The electrophysiological evaluation was performed on the 3rd week in sagittal cortico-striatal slices. (b) A representative image showing the location of the light stimulation (top image) and stimulating electrodes (bottom image, highlighted in red). (c) Light intensity-induced striatal field postsynaptic currents in WT and HD mice with AAV-ChR2 expressed in M2 cortex. (d) The graph shows the time course of Figure 6 continued on next page
protocol on cortical afferents and compared the amplitude of evoked striatal fPSC (Figure 6d–e). Both, WT-YFP and WT-ChR2 mice, presented a significant decrease in the amplitude of evoked fPSC following the LTD protocol that lasted at least 30 min, indicating cortico-striatal LTD induction. LTD was also slightly induced in HD-YFP, but to a less extent than WT-YFP (Student’s t-test, p = 0.0150). In the same conditions, stable LTD was induced in HD-ChR2 animals to the same extent as WT mice. Two-way ANOVA showed a mice group/time interaction (F(273, 4277) = 1.573; p < 0.0001), time effect (F(91, 4277) = 111.9; p < 0.0001) and group effect (F(3,47) = 3.312; p = 0.0279) and main group effects showed differences between HD-YFP and HD-ChR2 (p = 0.04), as shown by Bonferroni post hoc test. Indeed, similar results were obtained when analyzing the average of the fPSC amplitude after TBS (Figure 6e). Here, two-way ANOVA showed a genotype/stimulation interaction (F(1,47) = 5.621; p = 0.0219), and Bonferroni’s post hoc test showed that optogenetic stimulation restored the ability to induce LTD in HD mice.

To examine whether improved cortico-striatal synaptic function correlated with plasticity changes, we evaluated spine density from Golgi-impregnated striatal MSNs (Figure 6f–g). Spine density in striatal MSNs from HD mice was reduced compared to WT mice, as previously shown for MSNs from 3-month-old YAC128 (Marco et al., 2013) and for hippocampal apical dendrites from R6/1 (Miguez et al., 2015). Repeated optogenetic stimulation increased spine density in HD mice, without altering spine density in WT mice, as indicated by two-way ANOVA with genotype (F(1,94) = 56.52; p < 0.001), stimulation (F(1,94) = 14.29; p < 0.0003) and interaction effect (F(1,94) = 11.77; p < 0.0009). Bonferroni post hoc comparisons showed significant differences between WT-YFP and HD-YFP (p < 0.0001), and between HD-YFP and HD-ChR2 (p < 0.0001), indicating that repeated stimulation of the cortico-striatal pathway restored spine density in the striatum of HD mice. Altogether, our results show that optogenetic M2-striatal stimulation induces persistent synaptic plasticity changes that could explain the behavioral improvements found in HD mice.

Discussion
Basal ganglia circuit dysfunction is the leading cause of motor abnormalities in HD. In particular, cortico-striatal disconnection has a prominent role in disease progression. Here we further characterized cortico-striatal functional alterations in the symptomatic HD mouse. Also, our data highlight that the M2-DLS pathway is profoundly compromised in our R6/1 mouse model of HD. Modulation of brain circuits using optogenetic tools has emerged as a promising therapeutic strategy in many neurological disorders, such as Parkinson (Gradinaru et al., 2009; Kravitz et al., 2010; Magno et al., 2019), stroke (Cheng et al., 2014; Tennant et al., 2017), and psychiatric disorders (Fuchikami et al., 2015). In this line, we aimed to restore circuit function in HD by increasing selected cortico-striatal activity in symptomatic mice. Indeed, we provide strong evidence that we can ameliorate HD symptoms in symptomatic HD mice by stimulating the M2 cortex-DLS pathway.
Cortico-striatal functional connectivity and glutamate transmission are reduced in HD mice

Our results indicate general cortico-striatal and thalamo-striatal functional connectivity deficits in HD mice, which are in line with previously described alterations in striatal inputs (Reiner and Deng, 2018). However, synaptic loss, as well as electrophysiological responses in cortico-striatal or thalamo-striatal circuits, are differentially affected in HD (Deng et al., 2013; Kolodziejczyk and Raymond, 2016; Parievska et al., 2017; Reiner and Deng, 2018). Also, topographically selective changes in the cortex explain the clinical heterogeneity found in HD. For example, larger primary motor cortex degeneration correlates with motor impairments while cingulate cortex degeneration correlates with predominant mood symptomatology (Estrada-Sánchez and Rebec, 2013; Rosas et al., 2008; Thu et al., 2010). Therefore, further understanding how specific inputs to the striatum are altered could help to better understand the progression of HD symptoms.

Indeed, the cortex comprises the primary source of striatal glutamate, however, whether its total levels are altered in HD remains unclear. Cortical and striatal metabolites, measured by $^1$H MRS, are known to be profoundly altered in symptomatic HD models (Zacharoff et al., 2012), and glutamate concentration, measured by GluCEST, is known to be reduced in different brain regions, including most of the basal ganglia nuclei involved in motor behavior (Pépin et al., 2016). In our R6/1 mouse model, we also obtained divergent results. Brain metabolites, measured using $^1$H MRS, showed significant changes in line to the ones observed in Ki (Pépin et al., 2016), R6/2 (Tkac et al., 2007), and in vitro MRS striatal extracts from R6/2 mice (Jenkins et al., 2000). However, when evaluating absolute glutamate values by $^1$H MRS as well as baseline glutamate levels using microdialysis, we failed to show total glutamate alterations in the striatum of HD mice, in line with the unaltered glutamate levels described in R6/2 mice (Zacharoff et al., 2012). Conversely, GluCEST values indicate reduced glutamate concentration in both striatum and cortical regions. While further studies are needed to clarify alterations of total glutamate levels (which includes non-synaptic sources [Ramadan et al., 2013; van der Zeyden et al., 2008]); the glutamate/glutamine ratio (whose value is linked to functional/released synaptic glutamate) is consistently reduced in the striatum of HD mice, indicating that glutamatergic neurotransmission is defective in HD.

We then evaluated glutamate release from cortical terminals. Optogenetic stimulation of cortical afferents in the striatum induced a small glutamate increase in WT mice but failed to detect increases in glutamate (over baseline levels) in HD mice, indicating deficits in glutamate release in symptomatic stages. This effect is further supported by the blunted electrophysiological response to M2 optogenetic acute stimulation observed in the striatum of HD mice. Although previous work described higher glutamate release in R6/1 mice (Nicnicoall et al., 2001), these discrepancies could be explained by the different location of the microdialysis probe (dorsomedial striatum [DMS] versus DLS), mice age (16 versus 20 week-old-mice), and strategy to induce glutamate release (application of KCl at high concentration or NMDA versus selective optogenetic stimulation), which makes challenging to evaluate and compare sources of the glutamate measured (cortico-striatal versus thalamic or even astrocytic).

Moreover, convergent evidence indicates impaired glutamate release in HD, although most of them rely on electrophysiological measurements (Estrada-Sánchez and Rebec, 2013; Klapstein et al., 2001; Milnerwood and Raymond, 2007). Indeed, the monitoring of synaptic changes during the progression of HD in the YAC128 model reported biphasic age-dependent alterations of the cortico-striatal activity. Asymptomatic HD mice present increased glutamate release, postsynaptic currents, and synaptic responses. However, there is a shift in the three parameters as symptoms appear, which are maintained at late stages. Thus, symptomatic YAC128 mice exhibit reduced glutamate release, postsynaptic currents, and synaptic responses. Altogether, these data indicate that reduced glutamate release from the cortex, at least in late stages of the disease, might lead the basal ganglia network alterations found in HD patients.

Motor alterations in HD involve M2 cortex-DLS cortico-striatal dysfunction

Motor learning and coordination have been extensively characterized in animal models of HD (Creus-Muncunill et al., 2019; Hong et al., 2012; Puigdellívol et al., 2015). In this work, we support the idea that M2-DLS activity is necessary for the proper execution of motor learning and
coordination tasks, as by manipulating this specific cortico-striatal subcircuit we restore motor defects in pathological HD mice. Indeed, M2 lesions impair acquisition and reversal of a simple sequence consisting of two lever presses, one distal and the other proximal to reward (Yin, 2009). Also, there is an extensive functional reorganization in the striatum during different phases of learning during a motor learning task, such as accelerated rotarod (Yin, 2009) or serial order task (Rothwell et al., 2015). This includes initial predominant activity in DMS during early training, while extensive training engages DLS, indicating that DLS has a crucial role in the completion of a learned sequence (Rothwell et al., 2015; Yin, 2009). Moreover, the activity of MSNs from direct or indirect output pathways in the DLS also experiences divergent firing patterns during a motor learning task (Jin et al., 2014). Action initiation correlates to increased activity in both dMSNs and iMSNs in DLS, and, as the action sequence progress, most iMSNs reduce firing rate while dMSNs exhibit sustained activity (Jin et al., 2014; Rothwell et al., 2015). Taking this together, we suggest that our M2-DLS optogenetic stimulation might strengthen the ability to complete a motor learning task in HD mice.

In this line, the proportion of cortico-striatal inputs to the direct or indirect pathways depends on the cortical subregion from where these inputs arise (Wall et al., 2013). For example, the primary motor cortex sends axonal projections to a greater extent to the indirect pathway, while the sensory cortex projects more to the direct pathway, and the secondary motor cortex projects similarly to both striatal output circuits (Wall et al., 2013). Besides, cortical sparse long-range GABAergic projection neurons also modulate striatal output and motor behavior (Melzer et al., 2017; Rock et al., 2016). Specifically, somatostatin, but not PV, GABAergic neurons from M2 inhibit movement by both D1 and D2 MSNs inhibition, while somatostatin GABA long-range projections from M1 increase movement by inhibiting cholinergic interneurons in the striatum (Melzer et al., 2017). Thus, there is an urgent need to precisely map region and cell-specific striatal inputs to understand the functional organization of the cortico-striatal subcircuits and their impact on behavior, both under physiological and pathological conditions.

**Repeated M2 cortex-DLS stimulation leads to sustained synaptic plasticity changes and rectifies motor deficits in HD**

Our data demonstrate that selective optogenetic stimulations induce long-lasting effects in neuronal plasticity and behavior, which are fundamental for brain rewiring in pathological conditions. Optogenetic stimulation of the infralimbic prefrontal cortex induces sustained antidepressant behavioral and synaptic effects (i.e. spine density; Fuchikami et al., 2015), and optogenetic stimulation of the motor cortex promotes functional recovery after stroke (Cheng et al., 2014). Also, repeated cortico-striatal optogenetic stimulation generates persistent stereotypic behavior in mice (Ahmari et al., 2013) that lasts at least 2 weeks, which is specifically dependent on the cortico-striatal subcircuit stimulated (i.e. orbitofrontal cortex [OFC]–ventromedial striatum [VMS]; Ahmari et al., 2013). In contrast to our results, OFC–VMS stimulation induces grooming behavior in mice (Ahmari et al., 2013), pointing out that the specific effects are dependent on the distinct cortico-striatal subcircuits.

More surprising was the finding that M2-DLS stimulation was able to ameliorate exploratory behavior and stereotypies in HD mice. Our data show a decrease in rearing and an increase in stereotypic grooming time in our R6/1 mice compared to WT, as was previously observed in KI mice (Hong et al., 2012; Pépin et al., 2016). Also, we were able to induce exploratory activity, measured as rearing time, and reduce stereotypic grooming in already symptomatic mice by M2-DLS optogenetic stimulation. Active exploration and grooming modulate cortico-striatal phase synchrony in R6/2 mice (Hong et al., 2012), indicating that cortico-striatal function is involved in these behaviors. Here we further demonstrate that these spontaneous behaviors can be modulated by the M2-DLS pathway, and again, the effects are persistent at least 1 week, as changes are already observed before the light stimulation over the sessions. Therefore, optogenetic manipulations at cortical circuits generate sustained synaptic plasticity changes. However, if the long-lasting effects are specific of cortical circuits or are a general feature of optogenetic stimulation remains to be determined.

Overall, we highlight cortico-striatal circuits to be deeply altered in symptomatic HD mice. Moreover, by taking advantage of optogenetic techniques, we demonstrated altered glutamate release from M2 cortical projection neurons and deficient response in the striatum in HD. In future studies, the ability to dissect the function of different cortico-striatal subcircuits in physiological and pathological conditions might help to further understand how mHtt alters the information processing in the basal ganglia. Here, we highlight a key role of the M2 cortex-DLS specific subcircuit in the
modulation of motor alterations in HD, including exploratory behavior, stereotypies, motor learning, and coordination. In this context, we were able to successfully reestablish physiological, morphological, and behavioral alterations in our symptomatic HD mice by generating persistent synaptic plasticity in selected cortico-striatal circuits. Our successful approach opens new opportunities to design therapeutic strategies to ameliorate HD symptoms based on circuit restoration, which might be useful also for other basal ganglia disorders.

Materials and methods

Key resources table

| Reagent type (species) or resource | Designation | Source or reference | Identifiers | Additional information |
|-----------------------------------|-------------|---------------------|-------------|------------------------|
| Genetic reagent Mus musculus      | B6CBA-Tg(HDexon1) 61Gpb/1J (R6/1) | The Jackson Laboratory | RRID:IMSR_JAX:002809 | R6/1 HD model |
| Recombinant DNA reagent           | AAV1-CamKIIa-hChR2 (H134H)-eYFP-WPRE.hGH | University of Pennsylvania -Penn Vector Core |Catalog number: AV-1-26969P | titres: $8.97 \times 10^{12}$ genomic particles/mL (we used 1:10 dilution) |
| Recombinant DNA reagent           | AAV1-CamKIIa[1,3]-eYFP-WPRE.hGH; | University of Pennsylvania -Penn Vector Core |Catalog number: AV-1-PV2975 | titres: $1.18 \times 10^{13}$ genomic particles/mL (we used 1:10 dilution) |
| Software, algorithm               | GraphPad Prism software | GraphPad Prism (https://graphpad.com) | RRID:SCR_002798 | Version 8.0.0 |
| Software, algorithm               | Fiji        | https://imagej.net/Fiji | RRID:SCR_002285 | |
| Software, algorithm               | ANTs (Advanced Normalization ToolS) |http://stnava.github.io/ANTs/ | RRID:SCR_004757 | |
| Software, algorithm               | FSL         |http://www.fmrib.ox.ac.uk/fsl/ | RRID:SCR_002823 | |
| Software, algorithm               | Python      |http://www.python.org/ | RRID:SCR_008394 | |
| Software, algorithm               | SPM         |http://www.fil.ion.ucl.ac.uk/spm/ | RRID:SCR_007037 | |
| Software, algorithm               | Nitime      |http://nipy.org/nitime/ | RRID:SCR_002504 | |
| Software, algorithm               | LCModel     |http://s-provencher.com/pages/lcmodel.shtml | RRID:SCR_014455 | |
| Software, algorithm               | ITK-Snap    |http://www.nitrc.org/projects/itk-snap/ | RRID:SCR_002010 | |

Animals

R6/1 transgenic mice expressing exon-1 of mutant huntingtin containing 115 CAG repeats were acquired from The Jackson Laboratory (Bar Harbor, ME) and maintained in a B6CBA background. Genotypes were obtained by polymerase chain reaction (PCR) from tail biopsy and WT littermates were used as the control group. Animals were housed together in groups of mixed genotypes in a room kept at 19–22°C and 40–60% humidity under a 12:12 hr light/dark cycle with access to water and food ad libitum, and data were recorded for analysis by microchip mouse number. All animal procedures were approved by the animal experimentation Ethics Committee of the Universitat de Barcelona (274/18) and Generalitat de Catalunya (10101), in compliance with the Spanish RD 53/2013 and European 2010/63/UE regulations for the care and use of laboratory animals.

MRI image acquisition

11 WT mice and 13 R6/1 mice were scanned blind to the experimenter at 17–20 weeks of age on a 7.0T BioSpec 70/30 horizontal animal scanner (Bruker BioSpin, Ettlingen, Germany), equipped with an actively shielded gradient system (400 mT/m, 12 cm inner diameter). Each animal underwent two acquisition sessions. The first session included magnetic resonance spectroscopy (MRS) and CEST (chemical exchange saturation transfer) acquisition to assess metabolite concentration. The second
session was performed one week later and included structural T2-weighted imaging and resting-state functional magnetic resonance (rs-fMRI) to evaluate connectivity between regions of interest. In both cases, animals were placed in a supine position in a Plexiglas holder with a nose cone for administering anesthetic gases and were fixed using tooth and ear bars and adhesive tape. Animals were anesthetized with 2.5% isoflurane (70:30 N₂O:O₂). In the second session, a combination of medetomidine (bolus of 0.3 mg/kg, 0.6 mg/kg/h infusion) and isoflurane (0.5%) was used to sedate the animals.

In both sessions, 3D-localizer scans were used to ensure the accurate position of the head at the isocenter of the magnet. During the first session, MRS was acquired using PRESS (voxel size 5.4 μL, TR = 5000 ms, TE = 12 ms, 256 averages, partial water suppression, VAPOR) in a voxel located in the left striatum (*Figure 2a*). Voxel position was defined using T2 RARE images acquired in axial, sagittal, and coronal orientation as reference. A non-suppressed reference water signal was also acquired in the same voxel (eight averages). GluCEST and WASSR (water saturation shift referencing) were acquired from one coronal slice with a slice thickness of 2.5 mm, covering striatum and cortex. WASSR image was acquired as reference using a pulse of 500 ms and 0.5 μT with an offset range from -200 and 200 Hz. GluCEST sequence used a pulse of 6000 ms, 10 μT, and offset ranging from -1600 to 1600 Hz.

In the second session, a T2-weighted image was acquired using a RARE sequence with effective TE = 33 ms TR = 2.3 s, RARE factor = 8, voxel size = 0.08 × 0.08 mm², and slice thickness = 0.5 mm. rs-fMRI was acquired with an EPI sequence with TR = 2 s, TE = 19.4, voxel size 0.21 × 0.21 mm², and slice thickness 0.5 mm; 420 volumes were acquired resulting in an acquisition time of 14 min.

### Functional connectivity analysis

Two approaches were used to evaluate functional connectivity. On the one hand, whole-brain connectivity was evaluated using global network metrics (*Rubinov and Sporns, 2010*) and on the other hand, a seed-based analysis was performed to evaluate the connectivity of the striatum with the rest of the brain.

For both approaches, rs-fMRI was preprocessed, including slice timing, motion correction by spatial realignment using SPM8, correction of EPI distortion by elastic registration to the T2-weighted volume using ANTs (*Avants et al., 2008*), detrend, smoothing with a full-width half maximum (FWHM) of 0.6 mm, frequency filtering of the time series between 0.01 and 0.1 Hz and regression by motion parameters. All these steps were performed using NiTime ([http://nipy.org/nitime](http://nipy.org/nitime)).

The MRI-based atlas of the mouse brain (*Ma, 2008*) was considered for brain parcellation. To obtain more specific regions, the sensorimotor cortex defined in the original atlas was manually divided into somatosensory, orbitofrontal (OFC), motor 1 and 2 (M1, M2), cingulate, medial prefrontal cortex (mPFC), and retrosplenial cortex. The atlas template was elastically registered to each subject T2-weighted volume using ANTs (*Avants et al., 2008*), and the resulting transformation was applied to the label map to obtain the individual brain parcellation.

Region parcellation was registered from the T2-weighted volume to the preprocessed mean rs-fMRI. The whole-brain functional brain network was estimated considering the gray matter regions obtained by parcellation as the network nodes. Connectivity between each pair of regions was estimated as the Fisher-z transform of the correlation between average time series in each region. Network organization was quantified using graph metrics, namely, strength, global, and local efficiency, and average clustering coefficient (*Rubinov and Sporns, 2010*).

To perform the seed-based analysis, the striatum was selected from the automatic parcellation. The average time series in the seed was computed and correlated with each voxel time series, resulting in a correlation map describing the connectivity of striatum with the rest of the brain. The following regions of interest were identified from brain parcellation to evaluate their connectivity with the seed region: striatum, globus pallidus, thalamus, and cingulate, somatosensory cortices, M1, M2, mPFC, and OFC cortices. Connectivity was quantified as the mean value of the correlation map in each region, considering only positive correlations.

### Metabolite quantification

LC-Model (*Provencher, 1993*) was used to quantify the MRS-detectable metabolites in the striatum of mice, fitting a basis set of 19 small metabolites and nine macromolecules. Quality criteria were
defined for the whole spectrum as the FWHM lower than 0.06 ppm and the signal-to-noise ratio greater than 5. Also, metabolites quantified with relative Cramér-Rao lower bounds (CRLB) higher than 15% were discarded.

**GluCEST analysis**

To assess glutamate from CEST acquisition, in-home scripts in python were developed to process and quantify GluCEST asymmetry. GluCEST contrast was measured as the asymmetry between the image obtained with saturation at three ppm downfield from water (resonant frequency of exchangeable protons for glutamate) and the image with saturation at −3 ppm as follows (Cai et al., 2013; Cai et al., 2012):

\[
\text{GluCEST}_{\text{asym}} = \frac{100 \times M_{\text{sat}}(-3\text{ppm}) - M_{\text{sat}}(3\text{ppm})}{M_{\text{sat}}(-3\text{ppm})}
\]

To quantify and compare GluCEST asymmetry, the ventricles were manually delineated in each GluCEST map and the minimum asymmetry value in this region was taken as a reference value to subtract from the whole-brain map. Average regional GluCEST asymmetry relative to ventricles was computed in manually delineated regions (Figure 2d), namely, right and left striatum, and right and left cortex values were averaged.

**Stereotaxic surgery**

Stereotaxic surgery was performed in 16-week-old mice under isoflurane anesthesia (5% induction, and 1.5% maintenance). For optogenetic modulation, an adeno-associated virus (AAV) containing Channelrhodopsin (ChR2) under CaMKII promotor was injected (AAV1-CaMKIIa-hChR2(H134H)-eYFP-WPRE.hGH; AAV-ChR2) and a control YFP construct (AAV1-CaMKIIa-eYFP-WPRE.hGH; AAV-YFP) was used as control. Virus production, amplification, and purification were performed by University of Pennsylvania-Penn Vector Core (titers: \(\sim 1 \times 10^{12}\) genomic particles/mL) and a volume of 0.5 μL of corresponding viral constructs was injected bilaterally in M2 cortex at the following coordinates: +2.46 anteroposterior (AP), ±1 mediolateral (L), and −0.8 mm dorsoventral (DV) from bregma and dura mater, using 5 μL Hamilton syringe with a 33 gauge needle at 0.1 μL/min. The injection needle was left for an additional 5 min period to allow diffusion of virus particles and avoid reflux.

For in vivo optogenetic stimulation, additional fiber-optic cannulas (MFC_200/240–0.22_3.5_ZF1.25_FLT; Doric Lenses) were placed bilaterally in the striatum at AP +0.14, L ± 2.2, DV −3 mm from bregma and dura mater and secured using dental cement. Optogenetic stimulation and behavioral testing were performed 4 weeks later.

For microdialysis experiments, AAV-YFP or AAV-CHR2 virus constructs were injected in the M2 as described above 4 weeks before the microdialysis procedure. After 4 weeks, one concentric dialysis probe equipped with a Cuprophan membrane (1.5 mm long) was implanted in the dorsal striatum at coordinates (in mm, from bregma and skull): AP −1.1 (with a 20° angle); L 2.2; DV - 4.5 from dura mater, in anesthetized mice (isoflurane, 5% induction and 1.5% maintenance). Additional bilateral fiber-optic cannulas were implanted as described above.

**Optogenetic stimulation**

The blue light was delivered from 473 nm diode-pumped solid-state blue laser (Laserglow) at 10 Hz, 5 ms pulse width, and ~5 mW (measured at the end of the patchcord) using a custom-made waveform generator (Arduino). For in vivo experiments, mice were habituated to be connected to the fiber optic patch cord (Doric Lenses) before the experiment. Zirconia sleeves (Doric Lenses) were used to connect the patch cord to the fiber-optic cannulas.

For electrophysiological recordings, the fiber optic patch cord was placed above the slice surface.

**In vivo microdialysis**

Extracellular glutamate (Glu) levels were measured by in vivo microdialysis as previously described (López-Gil et al., 2007). Microdialysis experiments were performed in freely moving mice 24 hr (day 1) and 48 hr (day 2) after surgery. The artificial cerebrospinal fluid (aCSF) was pumped at 1.65 μL/min and dialysate samples were collected every 6 min in micro vials. Following an initial 3 hr
stabilization period, six baseline samples were collected before 1 min optogenetic stimulation (sample 7, day 1) and 5 min stimulation (sample 7, day 2). Glutamate concentration was analyzed by a blind experimenter using an HPLC consisting in a Waters 717plus autosampler and a Waters 600 quaternary gradient pump, and a Phenomenex Gemini 5 μm 100 × 3 mm column. Dialysate samples were pre-column derivatized with OPA reagent by adding 90 μL distilled water to the 10 μL dialysate sample and followed by the addition of 15 μL of the OPA reagent. After 2.5 min reaction, 80 μL of this mixture was injected into the column. Glutamate was detected with a Waters 2475 Fluorescence detector using excitation and emission wavelength of 360 and 450 nm, respectively. Following sample collection, mice were sacrificed, their brains were removed, sectioned, and stained with neutral red to ensure proper probe placement.

Multi-electrode arrays

Mouse brain sagittal sections were obtained on a vibratome (Microm HM 650 V, Thermo Scientific, Waltham, MA) at 350 µm thickness in oxygenated (95% O₂, 5% CO₂) ice-cold artificial cerebrospinal fluid (aCSF) containing (in mM) 124 NaCl, 24 NaHCO₃, 13 glucose, 5 HEPES, 2.5 KCl, 2.5 CaCl₂, 1.2 NaH₂PO₄, 1.3 MgSO₄. Slices were then transferred to an oxygenated 32°C recovery solution of the following composition (in mM): 92 NMDG, 30 NaHCO₃, 25 glucose, 20 HEPES, 10 MgSO₄, 5 sodium ascorbate, 2.5 KCl, 1.2 NaH₂PO₄, 3 sodium pyruvate, 2 thiourea, and 0.5 CaCl₂; for 15 min (Choi et al., 2019). Then, slices were transferred to oxygenated aCSF at room temperature and left for at least 1 hr before recording.

Following recovery, slices were placed in a multi-electrode array (MEA) recording dish, fully submerged in oxygenated aCSF at 37°C. Electrophysiological data were recorded by a blind experimenter with MEA set-up from Multi Channel Systems MCS GmbH (Reutlingen, Germany) composed of 60 channels USB-MEA60-inv system with a blanking unit from Multi Channel Systems and the STG4004 current and voltage generator. Experiments were carried out with 60MEA200/30iR-ITO MEA dishes consisting of 60 planar electrodes arranged in an 8 × 8 array (200 µm distance between neighboring electrodes and an electrode diameter of 30 µm). The software for stimulation, recording, and signal processing were MC Stimulus and MC Rack from Multi Channel Systems. Using a digital camera during recording assessed the position of the brain slices on the electrode field and the location of the laser for stimulation.

Striatal field post-synaptic currents (fPSC) were recorded in the dorsal striatum in response to the stimulation of cortical afferents with short laser pulses of increasing intensity. Light stimulation was performed by placing the laser in the slice approximately 0.5 mm posterior to bregma, 2.5 mm ventral from the surface, and 3 mm lateral from the midline (Figures 3d–e and 6a). The evoked striatal fPSCs were analyzed after trains of 1 ms light stimuli of increasing intensity (0.00, 0.08, 1.5, 5.6, 13.7, 28.7, 47.7, and 60 mW/mm²).

For electrical stimulation, we set one MEA electrode located approximately at 1 mm anterior to bregma, 2.5 mm depth from the brain surface and 2.2 mm lateral from the midline as stimulation one (Figure 6a, panel right), and fPSC were evoked by single monopolar biphasic pulses (negative/positive, 100 μs per phase). For input/output curves, cortico-striatal fibers were stimulated with trains of three positive-negative identical pulses at increasing currents (5 s inter-pulse time; 30 s train intervals; 250–3000 μV currents). Then, the pulse amplitude of subsequent stimuli was set to evoke 40% of the saturating fPSC response in the input/output curve. Long-term depression (LTD) was induced by theta-burst stimulation (TBS) consisting of 10 trains spaced 15 s apart. Each train consisted of 10 bursts at 10.5 Hz (theta), and each burst consisted of four stimuli at 50 Hz. Thus, the whole TBS stimulation period lasted 2.5 min (Hawes et al., 2013). In all cases, the amplitude of the evoked fPSC was quantified. Software for recording and signal processing was MC Rack from Multi Channel Systems. Using a digital camera during recording assessed the position of the brain slices on the electrode field.

Behavioral assessment

All behavioral tests were performed as previously described (Creus-Muncunill et al., 2019; Puigdellívol et al., 2015). Tests were done during the light phase and animals were habituated to the experimental room for at least 1 hr before testing. The apparatus was thoroughly cleaned between tests and animals. The order of the tests and time between tests is detailed in Figure 4d.
Open field
Spontaneous locomotor activity and exploratory behavior were assessed in an open field (OF) at weeks 20, 21, and 22 of age. The OF test was performed using a white square arena (40 × 40 × 30 cm³) with dim light (~20 lux). Mice were left in the center of the apparatus and allowed to explore the arena for 11 min. Optogenetic stimulation was performed from 5 to 6 min of the test. Animals were tracked and recorded with SMART 3.0 software (Panlab). The number of events and time spent doing rearing and grooming were measured to assess exploratory and stereotypic behavior.

Accelerating rotarod
Mice were placed on a motorized rod (30 mm diameter) with a rotation speed gradually increased from 4 to 40 rpm over 5 min and the latency to fall was recorded to assess motor learning (Creus-Muncunill et al., 2019). The procedure was performed four times per day with 1 hr inter-trial interval for 3 consecutive days, 12 trials in total.

Balance beam
Motor coordination and balance were determined by measuring the ability of the mice to traverse a narrow beam according to Creus-Muncunill et al., 2019. The beam consisted of a wooden square bar (50 cm long with 1.3 cm face), divided by 5 cm-frames and placed horizontally 50 cm above the bench surface, with each end mounted on narrow support. Animals could walk for 2 min along the beam and the number of frames crossed was measured.

Golgi stain and dendritic spine quantification
Fresh brain hemispheres were processed using the Rapid GolgiStain Kit (FD Neurotechnologies), as previously described (Alvarez-Periel et al., 2018). Bright-field images Golgi-impregnated MSNs striatal neurons from 100 µm brain slices were captured by a blind experimenter using a Leica epifluorescence microscope (×63 oil objective, magnification 1,6). Image Z stacks were taken every 0.2 µm and analyzed with Fiji software. Dendritic segments were traced (>20 µm long; average, 47.35 µm; mean range, 20–95 µm), and the spines were counted. Spine density was calculated in three to thirteen dendrites per neuron, and the values were averaged to obtain the mean for each neuron (7–11 different neurons per animal, n = 3 for WT-YFP, WT-ChR2, and HD-YFP, and n = 2 for HD-ChR2).

Statistical analysis
All data are expressed as mean ± SEM. Each point represents data from an individual mouse. Statistical analysis was performed using the two-tailed unpaired Student’s t-test or two-way ANOVA, and Bonferroni post hoc test as indicated in the figure legends. Values of p<0.05 were considered as statistically significant.

Acknowledgements
We are very grateful to Ana López (María de Maeztu Unit of Excellence, Institute of Neurosciences, University of Barcelona, MDM-2017–0729, Ministry of Science, Innovation, and Universities) and Maite Muñoz for their excellent technical support. This work has been funded by the Spanish Ministry of Sciences, Innovation and Universities through projects no. SAF2017-88076-R, RETICS de Terapia Celular, Instituto de Salud Carlos III (RD06/0010/0006), and la Marató de TV3. This research is part of NEUROPA. The NEUROPA Project has received funding from the European Union’s Horizon 2020 Research and Innovation Program under Grant Agreement No. 863214.

Additional information

| Funder                          | Grant reference number | Author      |
|---------------------------------|------------------------|-------------|
| Spanish Ministry of Sciences, Innovation and Universities | SAF2017-88076-R | Jordi Alberch |
| Instituto de Salud Carlos III  | RETICS (RD06/0010/0006) | Jordi Alberch |
The funders had no role in study design, data collection and interpretation, or the decision to submit the work for publication.

Author contributions
Sara Fernández-García, Data curation, Formal analysis, Funding acquisition, Validation, Investigation, Methodology, Writing - original draft, Writing - review and editing; Sara Conde-Berriozabal, Data curation, Formal analysis, Funding acquisition, Investigation, Methodology, Writing - review and editing; Esther García-García, Data curation, Funding acquisition, Methodology, Writing - review and editing; Clara Gort-Paniello, Investigation, Methodology, Writing - review and editing; David Bernal-Casas, Data curation, Supervision, Validation, Investigation, Writing - review and editing; Gerardo García-Díaz Barriga, Conceptualization, Investigation, Methodology; Javier López-Gil, Investigation, Methodology; Emma Muñoz-Moreno, Data curation, Software, Formal analysis, Validation, Writing - review and editing; Guadalupe Soria, Software, Supervision, Validation, Writing - review and editing; Leticia Campa, Formal analysis, Methodology, Writing - review and editing; Francesc Artigas, Resources, Supervision, Funding acquisition, Writing - review and editing; Manuel José Rodríguez, Data curation, Formal analysis, Validation, Investigation, Methodology, Writing - review and editing; Jordi Alberch, Conceptualization, Resources, Supervision, Funding acquisition, Validation, Project administration, Writing - review and editing; Mercè Masana, Conceptualization, Resources, Data curation, Formal analysis, Supervision, Funding acquisition, Validation, Investigation, Methodology, Writing - original draft, Writing - review and editing

Author ORCIDs
Sara Fernández-García https://orcid.org/0000-0003-2281-4526
Sara Conde-Berriozabal https://orcid.org/0000-0002-3712-8046
Esther García-García https://orcid.org/0000-0003-3997-493X
Clara Gort-Paniello https://orcid.org/0000-0003-3850-918X
Emma Muñoz-Moreno https://orcid.org/0000-0003-2104-7265
Guadalupe Soria https://orcid.org/0000-0002-8344-0479
Manuel José Rodríguez https://orcid.org/0000-0002-4476-004X
Jordi Alberch https://orcid.org/0000-0002-8684-2721
Mercè Masana https://orcid.org/0000-0003-1392-4774

Ethics
Animal experimentation: All animal procedures were approved by the animal experimentation Ethics Committee of the Universitat de Barcelona (274/18) and Generalitat de Catalunya (10101), in compliance with the Spanish RD 53/2013 and European 2010/63/UE regulations for the care and use of laboratory animals.

Decision letter and Author response
Decision letter https://doi.org/10.7554/eLife.57017.sa1
Author response https://doi.org/10.7554/eLife.57017.sa2
Additional files

Supplementary files
- Supplementary file 1. Average seed-based BOLD correlation maps from WT mouse striatum related to Figure 1b, visualized with ITK-SNAP software (Yushkevich et al., 2006).
- Supplementary file 2. Average seed-based BOLD correlation maps from R6/1 HD mouse striatum related to Figure 1b, visualized with ITK-SNAP software (Yushkevich et al., 2006).
- Transparent reporting form

Data availability
All data generated or analysed during this study are included in the manuscript and supporting files.

References
Ahmari SE, Spellman T, Douglas NL, Kheirbek MA, Simpson HB, Deisseroth K, Gordon JA, Hen R. 2013. Repeated cortico-striatal stimulation generates persistent OCD-like behavior. Science 340:1234–1239. DOI: https://doi.org/10.1126/science.1234733, PMID: 23744948

Alvarez-Periel E, Puigdollivol M, Brito V, Plattern F, Bibb JA, Alberch J, Ginés S. 2018. Cdk5 contributes to Huntington’s Disease Learning and Memory Deficits via Modulation of Brain Region-Specific Substrates. Molecular Neurobiology 55:6250–6268. DOI: https://doi.org/10.1007/s12035-017-0828-4, PMID: 29288339

Avants BB, Epstein CL, Grossman M, Gee JC. 2008. Symmetric diffeomorphic image registration with cross-correlation: evaluating automated labeling of elderly and neurodegenerative brain. Medical Image Analysis 12:26–41. DOI: https://doi.org/10.1016/j.media.2007.06.004, PMID: 17659998

Bagga P, Pickup S, Crescenzi R, Martínez D, Borthakur A, D’Aquilla K, Singh A, Verma G, Detre JA, Greenberg J, Hariharan H, Reddy R. 2018. In vivo GluCEST MRI: reproducibility, background contribution and source of glutamate changes in the MPTP model of Parkinson’s disease. Scientific Reports 8:2883. DOI: https://doi.org/10.1038/s41598-018-21035-3, PMID: 29440753

Belam JP, Hanley JJ, Booth PA, Bevan MD. 2000. Synaptic organisation of the basal ganglia. Journal of Anatomy 196 (Pt 4):527–542. DOI: https://doi.org/10.1046/j.1469-7580.2000.19640527.x, PMID: 10923985

Burgold J, Schulz-­Trieglaff EK, Voelkl K, Gutiérrez-­Ángel S, Bader JM, Hosp F, Mann M, Arzheimer T, Klein R, Liebscher S, Dudanova I. 2019. Cortical circuit alterations precede motor impairments in Huntington’s disease mice. Scientific Reports 9:43024. DOI: https://doi.org/10.1038/s41598-019-43024-w

Cai K, Haris M, Singh A, Kogan F, Greenberg JH, Hariharan H, Detre JA, Reddy R. 2012. Magnetic resonance imaging of glutamate. Nature Medicine 18:302–306. DOI: https://doi.org/10.1038/nm.2615, PMID: 22270722

Cai K, Singh A, Roalf DR, Nanga RP, Haris M, Hariharan H, Gur R, Reddy R. 2013. Mapping glutamate in subcortical brain structures using high-resolution GluCEST MRI. NMR in Biomedicine 26:1278–1284. DOI: https://doi.org/10.1002/nbm.2949, PMID: 23539322

Calabresi P, Picconi B, Tozzi A, Ghiglieri V, Di Filippo M. 2014. Direct and indirect pathways of basal ganglia: a critical reappraisal. Nature Neuroscience 17:1022–1030. DOI: https://doi.org/10.1038/nn.3743, PMID: 25065439

Cepeda C, Hurst RS, Calvert CR, Hernández-­Echeagaray E, Nguyen OK, Jocoy E, Christian LJ, Ariano MA, Levine MS. 2003. Transient and progressive electrophysiological alterations in the corticostriatal pathway in a mouse model of Huntington’s disease. The Journal of Neuroscience 23:961–969. DOI: https://doi.org/10.1523/ JNEUROSCI.23-03-00961.2003, PMID: 12574425

Cepeda C, Wu N, André VM, Cummings DM, Levine MS. 2007. The corticostriatal pathway in Huntington’s disease. Progress in Neurobiology 81:253–271. DOI: https://doi.org/10.1016/j.pneurobio.2006.11.001, PMID: 17169479

Cheng MY, Wang EH, Woodson WJ, Wang S, Sun G, Lee AG, Arac A, Fenno LE, Deisseroth K, Steinberg GK. 2014. Optogenetic neuronal stimulation promotes functional recovery after stroke. PNAS 111:12913–12918. DOI: https://doi.org/10.1073/pnas.1404109111, PMID: 25136109

Choi K, Holly EN, Davatolhagh MF, Beier KT, Fuccillo MV. 2019. Integrated anatomical and physiological mapping of striatal afferent projections. European Journal of Neuroscience 49:623–636. DOI: https://doi.org/10.1111/ejnn.13829, PMID: 2939830

Creus-­Muncunill J, Badillos-­Rodriguez R, Garcia-­Forn M, Masana M, Garcia-­Diaz Barriga G, Guisado-­Corcoll A, Alberch J, Malagelada C, Delgado-­García J, Gruart A, Pérez-­Navarro E. 2019. Increased translation as a novel pathogenic mechanism in Huntington’s disease. Brain 142:3158–3175. DOI: https://doi.org/10.1093/brain/ awz220, PMID: 31365052

Cummings DM, Milnerwood AJ, Dallierac GM, Waights V, Brown JY, Vatsavayai SC, Hirst MC, Murphy KP. 2006. Aberrant cortical synaptic plasticity and dopaminergic dysfunction in a mouse model of Huntington’s disease. Human Molecular Genetics 15:2856–2868. DOI: https://doi.org/10.1093/hmg/ddi224, PMID: 16905556
Deng YP, Wong T, Bricker-Anthony C, Deng B, Reiner A. 2013. Loss of corticostriatal and thalamostriatal synaptic terminals precedes striatal projection neuron pathology in heterozygous Q140 Huntington’s disease mouse. *Neurobiology of Disease* **60**:89–107. DOI: https://doi.org/10.1016/j.nbd.2013.08.009

Dumas EM, van den Bogaard SJAJ, Hart EP, Soeter RP, van Buchem MA, van der Grond J, Rombouts SARB, Roos RAC. 2013. Reduced functional brain connectivity prior to and after disease onset in Huntington’s disease. *NeuroImage: Clinical* **2**:377–384. DOI: https://doi.org/10.1016/j.nic.2013.03.001

Estrada-Sánchez AM, Rebec GV. 2013. Role of cerebral cortex in the neuropathology of Huntington’s disease. *Frontiers in Neural Circuits* **7**:19. DOI: https://doi.org/10.3389/fncir.2013.00019

Franklin K, Paxinos G. 1997. *The Mouse Brain in Stereotaxic Coordinates*. San Diego, California: Academic Press.

Freeze BS, Kravitz AV, Hammad N, Berke JD, Kreitzer AC. 2013. Control of basal ganglia output by direct and indirect pathway projection neurons. *Journal of Neuroscience* **33**:18531–18539. DOI: https://doi.org/10.1523/JNEUROSCI.1278-13.2013, PMID: 24259575

Fuchikami M, Thomas A, Liu R, Wohleb ES, Land BB, DiLeone RJ, Aghajanian GK, Duman RS. 2015. Optogenetic stimulation of infralimbic PFC produces ketamine’s rapid and sustained antidepressant actions. *PNAS* **112**:8106–8111. DOI: https://doi.org/10.1073/pnas.1417281112, PMID: 26056286

Ghiglieri V, Campanelli F, Marino G, Natale G, Picconi B, Calabresi P. 2019. Corticostriatal synaptic plasticity alterations in the R6/1 transgenic mouse model of Huntington’s disease. *Journal of Neuroscience Research* **97**:24521. DOI: https://doi.org/10.1002/jnr.24521

Gradinaru V, Mogri M, Thompson KR, Henderson JM, Deisseroth K. 2009. Optical deconstruction of parkinsonian neural circuitry. *Science* **324**:354–359. DOI: https://doi.org/10.1126/science.1167093, PMID: 19299587

Gu X, Li C, Wei W, Lo V, Gong S, Li SH, Iwasato T, Itahara S, Li XJ, Mody I, Heintz N, Yang XW. 2005. Pathological cell-cell interactions elicited by a neuropathogenically active form of mutant huntingtin contribute to cortical pathogenesis in HD mice. *Neuron* **46**:433–444. DOI: https://doi.org/10.1016/j.neuron.2005.03.025, PMID: 15882643

Hawes SL, Giliani F, Evans RC, Benkert EA, Blackwell KT. 2013. Sensitivity to theta-burst timing permits LTP in dorsal striatal adult brain slice. *Journal of Neurophysiology* **110**:2027–2036. DOI: https://doi.org/10.1152/jn.00115.2013, PMID: 23926032

Hintiryan H, Foster NN, Bowman I, Bay M, Song MY, Gou L, Yamashita S, Bienkowski MS, Zingg B, Zhu M, Yang XW, Shih JC, Toga AW, Dong HW. 2016. The mouse cortico-striatal projectome. *Nature Neuroscience* **19**:1100–1114. DOI: https://doi.org/10.1038/nn.4332, PMID: 27322419

Hong SI, Cossoy Leon D, Hussain WA, Walker LJ, Barton SJ, Rebec GV. 2012. Dysfunctional behavioral modulation of corticostriatal communication in the R6/2 mouse model of Huntington’s disease. *PLoS ONE* **7**:e47026. DOI: https://doi.org/10.1371/journal.pone.0047026, PMID: 23056565

Jenkins BG, Klivenyi P, Kustermann E, Andreassen OA, Ferrante RJ, Rosen BR, Beal MF. 2000. Nonlinear decrease over time in N-acetyl aspartate levels in the absence of neuronal loss and increases in glutamine and glucose in transgenic Huntington’s disease mice. *Journal of Neurochemistry* **74**:2108–2119. DOI: https://doi.org/10.1046/j.1471-4159.2000.0742108.x, PMID: 10809956

Jin X, Tecuapetla F, Costa RM. 2014. Basal ganglia subcircuits distinctively encode the parsing and concatenation of action sequences. *Nature Neuroscience* **17**:423–430. DOI: https://doi.org/10.1038/nn.3632, PMID: 24464039

Joshi PR, Wu NP, André VM, Cummings DM, Cepeda C, Joyce JA, Carroll JB, Leavitt BR, Hayden MR, Levine MS, Bamford NS. 2009. Age-dependent alterations of corticostriatal activity in the YAC128 mouse model of Huntington disease. *Neurobiology of Disease* **32**:286–297. DOI: https://doi.org/10.1016/j.nbd.2013.08.009, PMID: 19244517

Klapstein GJ, Fisher RS, Zanjani H, Cepeda C, Jokel ES, Chessee MF, Levine MS. 2001. Electrophysiological and morphological changes in striatal spiny neurons in R6/2 Huntington’s disease transgenic mouse. *Journal of Neurophysiology* **86**:2667–2677. DOI: https://doi.org/10.1152/jn.2001.86.6.2667, PMID: 11731527

Kolodziejczyk K, Raymond LA. 2016. Differential changes in thalamic and cortical excitatory synapses onto striatal spiny projection neurons in a Huntington disease mouse model. *Neurobiology of Disease* **56**:78–88. DOI: https://doi.org/10.1016/j.nbd.2015.11.020, PMID: 26621114

Kravitz AV, Freeze BS, Parker PR, Kay K, Thwin MT, Deisseroth K, Kreitzer AC. 2010. Regulation of parkinsonian motor behaviours by optogenetic control of basal ganglia circuitry. *Nature* **466**:622–626. DOI: https://doi.org/10.1038/nature09159, PMID: 20613723

Li W, Silva HB, Real J, Wang YM, Rial D, Li P, Payen MP, Zhou Y, Muller CE, Tomé AR, Cunha RA, Chen JF. 2015. Inactivation of adenosine A2A receptors reverses working memory deficits at early stages of Huntington’s disease models. *Neurobiology of Disease* **79**:70–80. DOI: https://doi.org/10.1016/j.nbd.2015.03.030, PMID: 25892655

López-Gil X, Babot Z, Amargós-Bosch M, Suhó C, Artigas F, Adell A. 2007. Clozapine and haloperidol differentially suppress the MK-801-increased glutamatergic and serotonergic transmission in the medial prefrontal cortex of the rat. *Neuropsychopharmacology* **32**:2087–2097. DOI: https://doi.org/10.1038/sj.npp.1301356, PMID: 17356574

Ma Y. 2008. In vivo 3D digital atlas database of the adult C57BL/6J mouse brain by magnetic resonance microscopy. *Frontiers in Neuroanatomy* **2**:8. DOI: https://doi.org/10.3389/neuro.05.001.2008

Magno LAV, Tenza-Ferrer H, Collodetti M, Aguiar MFG, Rodrigues APC, da Silva RS, Silva JDP, Nicolau NF, Rosa DVF, Birbrair A, Miranda DM, Romano-Silva MA. 2019. Optogenetic stimulation of the M2 cortex reverses motor dysfunction in a mouse model of Parkinson’s Disease. *The Journal of Neuroscience* **39**:3234–3248. DOI: https://doi.org/10.1523/JNEUROSCI.2277-18.2019, PMID: 30782975
Marco S, Giralt A, Petrovic MM, Pouladi MA, Martínez-Turrillas R, Martínez-Hernández J, Kaltenbach LS, Torres-Peraza J, Graham RK, Watanabe M, Lu Q, Nakaniishi N, Lipton SA, Lo DC, Hayden MR, Albert JH, Wesseling JF, Pérez-Otano I. 2013. Suppressing aberrant GluN3A expression rescues synaptic and behavioral impairments in Huntington's disease models. Nature Medicine 19:1030–1038. DOI: https://doi.org/10.1038/nm.3246, PMID: 23852340

Melzer S, Gil M, Koser DE, Michael M, Huang KW, Monyer H. 2017. Distinct corticostriatal GABAergic neurons mediate striatal output neurons and motor activity. Cell Reports 19:1045–1055. DOI: https://doi.org/10.1016/j.celrep.2017.04.024, PMID: 28467898

Míguez A, García-Díaz Barriga G, Brito V, Straccia M, Giralt A, Ginés S, Canals JM, Alberch J. 2015. Fingolimod (FTY720) enhances hippocampal synaptic plasticity and memory in Huntington's disease by preventing p75NTR up-regulation and astrocyte-mediated inflammation. Human Molecular Genetics 24:4958–4970. DOI: https://doi.org/10.1093/hmg/ddv218, PMID: 26063761

Milnerwood AJ, Raymond LA. 2007. Corticostriatal synaptic function in mouse models of Huntington's disease: early effects of huntingtin repeat length and synaptic load. The Journal of Physiology 585:817–831. DOI: https://doi.org/10.1113/jphysiol.2007.142448, PMID: 17947312

Niccoli B, Haraldsson B, Hansson O, O'Connor WT, Brundin P. 2001. Altered striatal amino acid neurotransmitter release monitored using microdialysis in R6/1 Huntington transgenic mice. European Journal of Neuroscience 13:206–210. DOI: https://doi.org/10.1046/j.1460-9568.2000.01379.x, PMID: 11933378

Pariv Breaks A, Moore C, Kamdjiou T, Cepeda C, Mosh CL, Levine M. 2017. Differential electrophysiological and morphological alterations of thalamostriatal and corticostriatal projections in the R6/2 mouse model of Huntington's disease. Neurobiology of Disease 108:29–44. DOI: https://doi.org/10.1016/j.nbd.2017.07.020, PMID: 28757327

Pépin J, Francelle L, Carrillo-de Sauvage MA, de Longprez L, Gipchtein P, Gambon K, Valette J, Brouillet E, Flament J. 2016. In vivo imaging of brain glutamate defects in a knock-in mouse model of Huntington's disease. NeuroImage 139:53–64. DOI: https://doi.org/10.1016/j.neuroimage.2016.06.023, PMID: 27318215

Provencher SW. 1993. Estimation of metabolite concentrations from localized in vivo proton NMR spectra. Magnetic Resonance in Medicine 30:672–679. DOI: https://doi.org/10.1002/mrm.1910300604, PMID: 8139448

Puigdollivel M, Cherubini M, Brito V, Giralt A, Suelves N, Ballesteros J, Zamora-Moratalia A, Martin ED, Epper BA, Alberch J, Gines S. 2015. A role for Kalarin-7 in corticostriatal synaptic dysfunction in Huntington's disease. Hum Mol Genet Ddv 1:ddv426. DOI: https://doi.org/10.1093/hmg/ddv426, PMID: 29582587

Ramadan S, Lin A, Stanwell P. 2013. Glutamate and glutamine: a review of in vivo MRS in the human brain. NMR in Biomedicine 26:1630–1646. DOI: https://doi.org/10.1002/nbm.3045, PMID: 24123328

Reiner A, Hart NM, Lei W, Deng Y. 2010. Corticostriatal projection neurons - dichotomous types and dichotomous functions. Frontiers in Neuroanatomy 4:142. DOI: https://doi.org/10.3389/fnana.2010.00142, PMID: 21088706

Reiner A, Deng YP. 2018. Disrupted striatal neuron inputs and outputs in Huntington's disease. CNS Neuroscience & Therapeutics 24:250–280. DOI: https://doi.org/10.1111/cns.12844, PMID: 29582587

Rocks C, Zurita H, Wilson C, Apicella AJ. 2016. An inhibitory corticostriatal pathway. eLife 5:e15890. DOI: https://doi.org/10.7554/eLife.15890, PMID: 27159237

Rosas HD, Salat DH, Lee SY, Zaleta AK, Pappu V, Fischl B, Greve D, Hevelone N, Hersch SM. 2008. Cerebral cortex and the clinical expression of Huntington's disease: complexity and heterogeneity. Brain 131:1057–1068. DOI: https://doi.org/10.1093/brain/awn025, PMID: 18337273

Rothwell PE, Hayton SJ, Sun GL, Fuccillo MV, Lim BK, Malenko RC. 2015. Input- and Output-Specific regulation of serial order performance by corticostriatal circuits. Neuron 88:345–356. DOI: https://doi.org/10.1016/j.neuron.2015.09.035, PMID: 26494279

Rubinov M, Sporns O. 2010. Complex network measures of brain connectivity: uses and interpretations. NeuroImage 52:1059–1069. DOI: https://doi.org/10.1016/j.neuroimage.2009.10.003, PMID: 19819337

Rueda-Orozco PE, Robbe D. 2015. The striatum multiplexes contextual and kinematic information to constrain motor habits execution. Nature Neuroscience 18:453–460. DOI: https://doi.org/10.1038/nn.3924, PMID: 25622144

Shepherd GM. 2013. Corticostriatal connectivity and its role in disease. Nature Reviews Neuroscience 14:278–291. DOI: https://doi.org/10.1038/nrn3469, PMID: 23511908

Tecuapetla F, Jin X, Lima SQ, Costa RM. 2016. Complementary contributions of striatal projection pathways to action initiation and execution. Cell 166:703–715. DOI: https://doi.org/10.1016/j.cell.2016.06.032, PMID: 27453468

Tennant KA, Taylor SL, White ER, Brown CE. 2017. Optogenetic rewiring of thalamostriatal circuits to restore function in the stroke injured brain. Nature Communications 8:15879. DOI: https://doi.org/10.1038/COMMUNICATIONS815879, PMID: 28643802

Thu DC, Oorschot DE, Tippett LJ, Nana AL, Hogg VM, Synek BJ, Luthi-Carter R, Waldvogel HJ, Faul RL. 2010. Cell loss in the motor and cingulate cortex correlates with symptomatology in Huntington's disease. Brain : A Journal of Neurology 133:1094–1100. DOI: https://doi.org/10.1093/brain/aws047, PMID: 20375136

Tkac I, Dubinsky JM, Keene CD, Gretert R, Low WC. 2007. Neurochemical changes in Huntington R6/2 mouse striatum detected by in vivo 1H MRS spectroscopy. Journal of Neurochemistry 100:1397–1406. DOI: https://doi.org/10.1111/j.1471-4119.2006.04323.x, PMID: 17217418

Unschuld PG, Joel SE, Liu X, Shanahan M, Margolis RL, Biglan KM, Bassett SS, Schretlen DJ, Redgrave GW, van Zijl PC, Pekar JJ, Ross CA. 2012. Impaired corticostriatal functional connectivity in Prodromal Huntington's disease. The Journal of Neuroscience 32:131

Fernández-Garcia et al. eLife 2020;9:e57017. DOI: https://doi.org/10.7554/eLife.57017
Disease. Neuroscience Letters 514:204–209. DOI: https://doi.org/10.1016/j.neulet.2012.02.095, PMID: 22425717

van der Zeyden M, Oldenziel WH, Rea K, Cremers TI, Westerink BH. 2008. Microdialysis of GABA and glutamate: analysis, interpretation and comparison with microsensors. Pharmacology Biochemistry and Behavior 90:135–147. DOI: https://doi.org/10.1016/j.pbb.2007.09.004, PMID: 17939932

Veldman MB, Yang XW. 2018. Molecular insights into cortico-striatal miscommunications in Huntington's disease. Current Opinion in Neurobiology 48:79–89. DOI: https://doi.org/10.1016/j.conb.2017.10.019, PMID: 29125980

Wall NR, De La Parra M, Callaway EM, Kreitzer AC. 2013. Differential innervation of direct- and indirect-pathway striatal projection neurons. Neuron 79:347–360. DOI: https://doi.org/10.1016/j.neuron.2013.05.014, PMID: 23810541

Wang N, Gray M, Lu XH, Cantle JP, Holley SM, Greiner E, Gu X, Shirasaki D, Cepeda C, Li Y, Dong H, Levine MS, Yang XW. 2014. Neuronal targets for reducing mutant huntingtin expression to ameliorate disease in a mouse model of Huntington's disease. Nature Medicine 20:536–541. DOI: https://doi.org/10.1038/nm.3514, PMID: 24784230

Yin HH. 2009. The role of the murine motor cortex in action duration and order. Frontiers in Integrative Neuroscience 3:23. DOI: https://doi.org/10.3389/neuro.07.023.2009, PMID: 19847323

Yushkevich PA, Piven J, Hazlett HC, Smith RG, Ho S, Gee JC, Gerig G. 2006. User-guided 3D active contour segmentation of anatomical structures: significantly improved efficiency and reliability. NeuroImage 31:1116–1128. DOI: https://doi.org/10.1016/j.neuroimage.2006.01.015, PMID: 16545965

Zacharoff L, Tkac I, Song Q, Tang C, Bolan PJ, Mangia S, Henry PG, Li T, Dubinsky JM. 2012. Cortical metabolites as biomarkers in the R6/2 model of Huntington’s disease. Journal of Cerebral Blood Flow & Metabolism 32:502–514. DOI: https://doi.org/10.1038/jcbfm.2011.157, PMID: 22044866

Zhang F, Gradinaru V, Adamantidis AR, Durand R, Airan RD, de Lecea L, Deisseroth K. 2010. Optogenetic interrogation of neural circuits: technology for probing mammalian brain structures. Nature Protocols 5:439–456. DOI: https://doi.org/10.1038/nprot.2009.226, PMID: 20203662