Evaluation of a novel lower radiation computed tomography protocol for assessment of tunnel position post anterior cruciate ligament reconstruction

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varun vasudeva  vasudeva.vv1@gmail.com
Darling Downs Hospital and Health Service
Corresponding Author
ORCiD: 0000-0003-1339-1533

Stephen Key
Gold Coast University Hospital

Alfred Phillips
Gold Coast University Hospital

Steve Kahane
Gold Coast University Hospital

Joseph Stevens
Gold Coast University Hospital

Chris Wall
Gold Coast University Hospital

Price Gallie
Gold Coast University Hospital

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Abstract

Background Anterior cruciate ligament (ACL) reconstruction is a common orthopaedic procedure. We developed a novel, low dose computed tomography (LDCT) protocol to assess tunnel position post-operatively. The effective radiation dose of this protocol is <0.5mSv, which is significantly less than the 2mSv dose for a conventional CT protocol. The aim of this study was to assess the accuracy of the LDCT protocol for determining tunnel position.

Methods Twenty-six patients who underwent primary ACL reconstruction were included in the study. A LDCT scan was performed six weeks post-operatively. Femoral and tibial tunnel positions were measured on three dimensional (3D) reconstructions using previously validated techniques. Measurements were performed independently by three observers at two time points, four weeks apart. Results There was excellent intra- and inter-rater reliability for all measurements using the images obtained from the LDCT protocol. Intra-class correlation coefficient (ICC) values were >0.9 for all measurements. Conclusions The LDCT protocol described in this study accurately demonstrates femoral and tibial tunnels post ACL reconstruction, while exposing the patient to a quarter of the radiation dose of a conventional CT. This protocol could be used by orthopaedic surgeons for routine post-operative imaging, in place of plain film radiographs.

Background

Rupture of the ACL is a common sporting injury [1]. ACL reconstruction is an effective orthopaedic procedure, allowing return to sporting activity after appropriate rehabilitation [2]. However, graft rupture is a common complication, occurring in up to 20% of cases, with younger patients being at higher risk [3]. A significant portion of graft ruptures may be attributed to technical error, specifically with improper bone tunnel placement [4, 5].
Suboptimal tunnel position results in increased risk of symptomatic knee instability and graft rupture, independent of graft type or tunnel preparation technique [6]. Tunnel position may be assessed post operatively using a number of imaging modalities. Plain film radiography is commonly used, with anteroposterior (AP) and lateral x-rays of the knee demonstrating the bony tunnels. A number of techniques have been proposed to determine correct tunnel position [7]. However, x-rays only provide a two dimensional (2D) image and hence may be difficult to interpret [7]. Computed tomography (CT) with 3D image reconstruction allows detailed assessment of osseous anatomy and has been shown to accurately demonstrate tunnel position [8, 9]. However CT has the disadvantage of a higher radiation dose to the patient.

We developed a novel LDCT protocol, with the goal of accurately assessing tunnel position post ACL reconstruction, while minimising radiation exposure to the patient. The purpose of this study was to evaluation the accuracy of this protocol in determining the femoral and tibial tunnel positions.

Methods

Patients undergoing isolated primary ACL reconstruction by the senior author (PG) over a 12-month period were prospectively recruited to the study. Paediatric patients (aged less than 18 years) and patients undergoing revision surgery were excluded. Ethics approval was obtained from our local research ethics committee, and all patients provided informed consent prior to inclusion in the study.

A single bundle ACL reconstruction was performed with a four-strand short graft, using the Tape Lock Screw technique (TLS®, FH Orthopaedics, Heimsbrunn, France) [10]. This technique utilises the ipsilateral semitendinosus tendon, which is fashioned into a four-strand closed loop (50-60mm in length, depending on height and gender) and pre-
tensioned to 500N for one minute. Femoral and tibial tunnels are created independently in a retrograde manner to match the diameter of each end of the graft. The tunnels are centred over the midpoint of the anatomic footprints of the native ACL. The graft is introduced using an all-inside technique, and secured with polyethylene terephthalate tapes passed through each end of the closed tendon loop and suspended in the bone tunnels with interference screws.

All patients underwent a standardised LDCT six weeks post operatively. The LDCT protocol involves a helical scan with 1mm thick slices, 128x0.6mm collimation, 80kVp and 80mAs (effective). A Siemens Definition AS+ CT scanner (Seimens Somatom Definition AS+; Siemens Healthcare, Forchheim, Germany) was used. Data was imported into Philips 2nd edition software (Philips Medical Systems North America, Shelton, Conn) to create a complete 3D volume reconstruction of each femur (to 10cm above the femoral condyle) and tibia (to 1cm below the tibial tubercle). The femoral 3D reconstruction had at least 90% overlap of femoral condyles and then virtual subtraction of the medial femoral condyle at the highest point of the intercondylar notch, leaving the most medial sagittal aspect of lateral femoral condyle with tunnel position on view (Figure 1). The tibial 3D reconstruction was an axial view, adjusted to view the most superior aspect of the proximal tibia with the femur and patella removed (Figure 2). The 3D reconstructions were imported into IntelliSpace Patient Archiving and Communication System (IntelliSpace PACS Enterprise; Philips) for measurement.

**Femoral Tunnel Measurement**

The quadrant method described by Bernard was used to assess femoral tunnel position (Figure 1) [11, 12]. Point A is the centre of the femoral tunnel on the medial aspect of the
lateral femoral condyle. A rectangular reference frame is superimposed. Distance B is the total sagittal diameter of the condyle, measured along the intercondylar notch roof, limited by the shallowest and deepest contours of the condyle. Distance C is the height of the intercondylar space, measured as the perpendicular distance between the notch roof and a parallel line tangential to the lowest point on the femoral condyle. Distance B and Distance C define the intercondylar space and create the axes for the quadrant system. Distance D is measured between Point A and the deep contour of the condyle, parallel to the notch roof. Distance E is the perpendicular distance between Point A and the notch roof. Femoral tunnel position in the sagittal plane is the defined by calculating ratios D/B and E/C.

**Tibial Tunnel Measurement**

The tibial tunnel position was assessed using a rectangular reference frame, as has been previously described (Figure 2) [12, 13]. The posterior border is drawn tangential to the posterior margins of the medial and lateral articular surfaces. The anterior border is drawn parallel to the posterior border, tangential to the anterior margin of the medial articular surface. The medial and lateral borders are drawn tangential to the most medial and lateral articular margins, respectively, perpendicular to the posterior border. Distance F is the mediolateral (ML) dimension of the tibial plateau. Distance G is the AP dimension of the tibial plateau. Point H is the centre of the tibial tunnel. Distance I and Distance J are measured perpendicularly from the medial and anterior borders of the reference frame, respectively. Tibial tunnel position is then defined in the axial plane by calculating ratios I/F and J/G.

**Statistics**
Femoral and tibial tunnel position was measured for each case independently by three observers (VV, SKe, SKa) at two time intervals, four weeks apart, in a blinded fashion. Images were de-identified and presented in random order, and the sequence was changed for the second measurement. Statistical analysis was performed using SPSS version 23.0 software (IBM Corp. IBM SPSS Statistics for Windows, Armonk, New York). Intra- and inter-rater reliability was calculated using a 2-way random absolute agreement model ICC and standard error of measurement (SEM). Single measures ICC was used to determine intra-rater reliability and average measures ICC was used to determine inter-rater reliability by comparing the means of 2 measurements of each variable.

Results

A total of 26 patients were included in the study. There were 15 females and 11 males with a mean age of 31 years (range 20 to 47 years). Femoral and tibial tunnel measurements and intra- and inter-rater ICC values are presented in Table 1. There was excellent intra- and inter-rater agreement for all measurements (ICC > 0.9) using the LDCT protocol. The effective radiation dose of the LDCT protocol was measured as <0.5 mSV and the expected uterine equivalent dose was <0.1 mSv. This compares to an average 1.99 mSv dose for a standard knee CT using the scanner at our institution.

Discussion

ACL reconstruction is a well-established treatment for ACL deficient patients, and the incidence of the procedure is increasing [1]. Surgeons often obtain post-operative imaging to assess the femoral and tibial tunnel positions. Plain film radiography and CT are the two commonly used modalities, and each has advantages and disadvantages. Plain film radiography is used by many surgeons to assess tunnel position, given its ease of access,
low cost, and low radiation exposure to the patient [25]. However, several studies have shown that CT scans, especially with 3D reconstruction, more accurately demonstrate the bony tunnels than standard orthogonal knee x-rays following primary ACL reconstruction [22,23]. Similarly, when considering revision ACL reconstruction, CT scans have also demonstrated superiority to plain radiographs in accurately assessing tunnel position [24]. CT imaging is becoming more readily available, however does come at the cost of a higher radiation dose to the patient [18].

Reported effective radiation doses for knee CT vary widely in the literature [14-16]. This likely reflects variations in equipment, protocols and intended applications. At our institution, a standard knee CT protocol exposes the patient to an average effective radiation dose of 1.99 mSv. Similarly, the effective radiation dose for orthogonal knee x-rays will vary from hospital to hospital [17]. At our institution, standard orthogonal knee x-rays expose the patient to an effective radiation dose of approximately 0.6µSv. The LDCT protocol presented in this study was developed to allow 3D measurement of bony tunnel position while minimizing radiation exposure to the patient. The effective radiation dose was measured at <0.5 mSv, which is a quarter of the radiation dose of a conventional CT. Despite the low radiation dose, this protocol allows accurate and reproducible 3D reconstructions with reliable visualisation of the femoral and tibial tunnels. This was demonstrated by the high intra- and inter-rater reliability of tunnel position measurements (ICC >0.9 for all measurements). No harmful effects of radiation exposure of <0.5mSv have been demonstrated [18]. The Australian Radiation Protection and Nuclear Safety Agency (ARPANSA) recommend no more than 5 mSv exposure per year [19]. The theoretical risk of cancer incidence for an exposure of 0.5mSV using age and sex specific factors in a 20-year-old male and female is 1:20,000 and 1:12,000 respectively [18].
theoretical cancer risk decreases with increasing patient age.

The major strength of this study is its applicability to clinical practice. All measurements were performed in CT scans of real patients performed post-operatively, with hamstring grafts and fixation devices in situ. This is in contrast to previously described cadaveric models [12]. We have demonstrated that a high degree of accuracy can be achieved using this protocol in a clinical setting. Furthermore, this study demonstrates that a high degree of accuracy can be achieved with this LDCT protocol by observers at different levels of surgical training. Two of the observers in this study were orthopaedic surgeons and one was a junior orthopaedic registrar. A high degree of inter-rater reliability was demonstrated for all measurements, despite the observers’ different levels of training. A single validated method was chosen to describe each bony tunnel, as the goal of this study was to determine the reliability of the LDCT protocol, rather than to evaluate the measurement methods themselves. Despite the quadrant method for femoral tunnel position originally being described for plain film radiographs, multiple studies have demonstrated high levels of intra- and inter-rater reliability when applied to 3D CT reconstructions [12, 20]. The current study supports these findings. Similarly, the described method for defining tibial tunnel placement has also been shown to be highly reliable in previous studies, as well as the current study [20]. Our results are comparable with those using standard CT protocols, indicating that the LDCT protocol is reliable for determining bony tunnel position [12, 13].

We acknowledge that this study has limitations. The sample size of 26 patients is small, however this is comparable with previously published studies validating tunnel position measurement protocols [8, 12, 21]. We intentionally did not include a control group
utilising a standard CT protocol. Previous studies have validated the measurement methods we used to determine femoral and tibial tunnel positions using standard CT protocols. Our outcome of interest was the accuracy of tunnel position measurement using the LDCT protocol, which we have clearly demonstrated. We felt that subjecting control patients to a higher radiation exposure was unjustified [8, 13]. The surgical technique used in this study attempts to place the ACL graft in an anatomic position, using the native femoral and tibial footprints as landmarks. It is possible that reconstruction techniques using alternative tunnel positions may not be reliably assessed using this LDCT protocol. Alternative 3D reconstructions may be required in such cases, and we cannot comment on the reliability of this protocol to demonstrate the tunnel positions.

Declaration

There was appropriate ethical approval given by the Gold Coast University Hospital Human Research Ethics Committee (reference number: HREC/15/QGC/119) to undergo this research and proceed to publication. All patients provided written consent to participate in this study and have their imaging used for publication which is available upon request. Data images and materials are available for further viewing and review if required by request of the corresponding author on reasonable request. The authors declare they have no competing interests. No funding was received for this study. AP completed the proposal and ethics application. JS collected the data, consented patients and provided the images. SKe and SKa were both authors who interpreted the data and made edits to the manuscript. VV wrote the manuscript and was the corresponding author for this study. CW made further edits and significant changes to this manuscript. PG was the supervisor for this study and aided throughout the process. Acknowledgement must be made to the radiology department at Gold Coats University Hospital who helped with acquiring the appropriate images.
Conclusion

The novel LDCT protocol described in this study provides 3D images which accurately demonstrate the bony anatomy of femoral and tibial tunnels following ACL reconstruction, while minimizing radiation exposure to the patient. We demonstrated excellent intra- and inter-rater reliability using previously validated measurement techniques. The radiation exposure to the patient using this LDCT protocol is a quarter of that experienced with a conventional CT. We believe this LDCT protocol could be used by orthopaedic surgeons for routine post-operative imaging of ACL tunnel position, in place of plain film radiographs.

Table 1

Table 1

*Measurements of femoral and tibial tunnel position and ICC values*
|                | Femoral | Tibia |  |
|----------------|---------|-------|---|
|                | D/B     | E/C   | J/G | I/F |
| Mean           | 0.337   | 0.270 | 0.437 | 0.468 |
| SD             | 0.077   | 0.083 | 0.0 | 0.026 |
| Min            | 0.154   | 0.086 | 0.2 | 0.389 |
| Max            | 0.500   | 0.506 | 0.5 | 0.534 |
|                |         |       |     |     |
| Inter-rater    |         |       |     |     |
| ICC            | 0.995   | 0.99  | 0.964 | 0.961 |
| Lower bound (95% CI) | 0.980 | 0.974 | 0.932 | 0.923 |
| Upper bound (95% CI) | 0.998 | 0.996 | 0.983 | 0.982 |
| SEM            | 0.005   | 0.008 | 0.012 | 0.005 |
|                |         |       |     |     |
| Intra-rater 1  |         |       |     |     |
| ICC            | 0.965   | 0.922 | 0.931 | 0.936 |
| Lower bound (95% CI) | 0.925 | 0.823 | 0.852 | 0.863 |
| Upper bound (95% CI) | 0.984 | 0.965 | 0.971 | 0.971 |
| SEM            | 0.014   | 0.023 | 0.016 | 0.007 |
|                |         |       |     |     |
| Intra-rater 2  |         |       |     |     |
| ICC            | 0.972   | 0.921 | 0.949 | 0.953 |
| Lower bound (95% CI) | 0.939 | 0.821 | 0.899 | 0.899 |
| Upper bound (95% CI) | 0.987 | 0.965 | 0.979 | 0.979 |
| SEM            | 0.013   | 0.023 | 0.014 | 0.006 |
|                |         |       |     |     |
| Intra-rater 3  |         |       |     |     |
| ICC            | 0.969   | 0.96  | 0.968 | 0.923 |
| Lower bound (95% CI) | 0.929 | 0.915 | 0.931 | 0.837 |
| Upper bound (95% CI) | 0.986 | 0.982 | 0.964 | 0.900 |
| SEM            | 0.013   | 0.017 | 0.016 | 0.007 |
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Figures
Figure 1

3D femoral reconstruction showing quadrant method to assess tunnel position
Figure 2

3D tibial reconstruction showing rectangular reference frame to assess tunnel position