Dosimetric benefit of MR-guided online adaptive radiotherapy in different tumor entities: liver, lung, abdominal lymph nodes, pancreas and prostate

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Abstract

Background: Hybrid magnetic resonance (MR)-Linac systems have recently been introduced into clinical practice. The systems allow online adaption of the treatment plan with the aim of compensating for interfractional anatomical changes. The aim of this study was to evaluate the dose volume histogram (DVH)-based dosimetric benefits of online adaptive MR-guided radiotherapy (oMRgRT) across different tumor entities and to investigate which subgroup of plans improved the most from adaption.

Methods: Fifty patients treated with oMRgRT for five different tumor entities (liver, lung, multiple abdominal lymph nodes, pancreas, and prostate) were included in this retrospective analysis. Various target volume (gross tumor volume GTV, clinical target volume CTV, and planning target volume PTV) and organs at risk (OAR) related DVH parameters were compared between the dose distributions before and after plan adaption.

Results: All subgroups clearly benefited from online plan adaption in terms of improved PTV coverage. For the liver, lung and abdominal lymph nodes cases, a consistent improvement in GTV coverage was found, while many fractions of the prostate subgroup showed acceptable CTV coverage even before plan adaption. The largest median improvements in GTV near-minimum dose (D98%) were found for the liver (6.3%, p < 0.001), lung (3.9%, p < 0.001), and abdominal lymph nodes (6.8%, p < 0.001) subgroups. Regarding OAR sparing, the largest median OAR dose reduction during plan adaption was found for the pancreas subgroup (-87.0%). However, in the pancreas subgroup an optimal GTV coverage was not always achieved because sparing of OARs was prioritized.

Conclusion: With online plan adaptation, it was possible to achieve significant improvements in target volume coverage and OAR sparing for various tumor entities and account for interfractional anatomical changes.

Keywords: Online MRI guided radiotherapy, Plan adaption, MRgOART, Online adaptive RT, MR-guided RT

Background

Various inter- and intra-fractional anatomical changes in patient anatomy pose a major challenge for the safe and successful treatment application in modern ablative image-guided radiotherapy (RT). Typical examples of such changes in patient geometry are different organ...
fillings of bladder, stomach or rectum, breathing-related motion, peristalsis, cardiac motion, tumor response (shrinkage), or organ and patient weight changes [1]. Numerous motion patterns of organs at risk (OAR), target volumes or quantification of motion amplitudes can be found in the literature [2–6].

These types of anatomical changes occur on various time-scales, ranging from seconds to weeks, and can potentially be accounted for via tumor-tracking or gating techniques and plan adaption strategies [1]. Although the technical implementation of such advanced RT techniques can be challenging, several adaptive RT (ART) approaches have found their way into clinical routine [1–7]. The feasibility and clinical benefit of offline ART using computed tomography (CT) or magnetic resonance imaging (MRI) has been demonstrated [8–12]. Strategies for online ART based on in-room cone-beam computed tomography (CBCT) have also been proposed [13–21]. A newly developed commercial CBCT-based system even allows for fast online ART in the clinical routine (Ethos™: Varian Medical Systems, Palo Alto, CA, USA) [22]. In this context, combined hybrid MR-Linac systems (e.g. MRIdian™: ViewRay Inc., Oakwood Village, OH, USA; or Unity™: Elekta AB, Stockholm, Sweden) have the advantage of superior soft-tissue contrast and dose-free intrafractional imaging (where available, also with real-time tumor tracking and gated RT) in addition to the technical implementation of such advanced RT techniques.

The feasibility and clinical benefit of adaptive RT (ART) using the MRIdian system (ViewRay Inc., Oakwood Village, OH, USA) with a step-and-shoot intensity modulated radiotherapy (IMRT) technique in the thoracic or abdominal region according to the institutional oMRgRT clinical protocol. The commercially available system consists of a hybrid MR-Linac and an integrated treatment planning system (TPS). Dose prescription referred to either the 65%, 80% or 95% isodose. Two patients were treated for two lesions simultaneously (patients 35 and 49) and one patient was treated for three lesions simultaneously (patient 42). In those three patients, the multiple lesions were treated with one single treatment plan. Thus, all OAR constraints of the corresponding fractions were counted as if these patients only had a single lesion. Parameters for target volumes (both gross tumor volume (GTV) and planning target volume (PTV)) were evaluated separately for each lesion. A total of 265 online adapted fractions were analyzed. Only fractions which were adapted were considered in the analysis.

The mean percentage of adapted fractions per patient was 86% (range 15% to 100%) and 79% of all fractions were adapted in total. Table 2 (Results) shows the portion of adapted plans and characteristics of the online adapted plans for each subgroup.

**oMRgRT workflow**

The oMRgRT workflow was similar to that described by Bohoudi et al. [2]. For initial treatment planning, a planning MR and CT were acquired using the same patient setup. The planning CT was acquired immediately after the MR. The CT was registered using deformable image registration (DIR) to the MR to obtain electron density values for dose calculation. GTV, clinical target volume (CTV) and OAR delineation was performed on the MR. In the TPS, Boolean operations of regions of interest (ROIs; e.g. subtraction or margin expansion of structures) can be performed and stored as so-called “rules”. Such rules were defined for the automatic generation of the PTV (expansion of the GTV) and derived structures were defined at the treating physician’s discretion to reduce the contouring effort during online adaptation. After dose prescription and contour delineation, a baseline treatment plan was generated analogous to the workflow in conventional RT. All plans were generated as step-and-shoot IMRT via inverse planning (6 MV flattening filter free beam; 1.5 mm calculation grid size with isotropic voxels; 1.0% Monte Carlo dose calculation uncertainty) and the maximum number of multi leaf collimator (MLC) segments was limited, depending on the complexity of the plan. This segment number limit of the baseline plan was subsequently used for online plan adaption. For each treatment fraction, a balanced steady-state free precession (bSSFP) pulse...
### Table 1  Patient characteristics

| Patient Nr | Nr. of lesions | Nr. of adapted fx | Total nr. of fx | Fraction dose (Gy) | Total dose (Gy) | Prescription (%) | Group   |
|------------|----------------|-------------------|----------------|--------------------|----------------|-----------------|---------|
| 1          | 1              | 3                 | 20             | 3                  | 60             | 95              | Prostate |
| 2          | 1              | 14                | 20             | 3                  | 60             | 95              | Prostate |
| 3          | 1              | 5                 | 5              | 7.25               | 36.25          | 95              | Prostate |
| 4          | 1              | 7                 | 20             | 3                  | 60             | 95              | Prostate |
| 5          | 1              | 20                | 20             | 3                  | 60             | 95              | Prostate |
| 6          | 1              | 19                | 20             | 3                  | 60             | 95              | Prostate |
| 7          | 1              | 20                | 20             | 3                  | 60             | 95              | Prostate |
| 8          | 1              | 16                | 20             | 3                  | 60             | 95              | Prostate |
| 9          | 1              | 9                 | 20             | 3                  | 60             | 95              | Prostate |
| 10         | 1              | 5                 | 5              | 7                  | 35             | 95              | Prostate |
| 11         | 1              | 2                 | 5              | 8                  | 40             | 95              | Pancreas |
| 12         | 1              | 4                 | 5              | 8                  | 40             | 95              | Pancreas |
| 13         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 14         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 15         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 16         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 17         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 18         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 19         | 1              | 5                 | 5              | 6.6                | 33             | 80              | Pancreas |
| 20         | 1              | 5                 | 5              | 8                  | 40             | 80              | Pancreas |
| 21         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 22         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 23         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 24         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 25         | 1              | 3                 | 3              | 15                 | 45             | 65              | Liver    |
| 26         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 27         | 1              | 2                 | 3              | 15                 | 45             | 65              | Liver    |
| 28         | 1              | 3                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 29         | 1              | 3                 | 3              | 15                 | 45             | 65              | Liver    |
| 30         | 1              | 2                 | 3              | 12.5               | 37.5           | 65              | Liver    |
| 31         | 1              | 5                 | 5              | 7                  | 35             | 95              | Lymph nodes |
| 32         | 1              | 4                 | 5              | 5                  | 25             | 80              | Lymph nodes |
| 33         | 1              | 2                 | 5              | 8                  | 40             | 95              | Lymph nodes |
| 34         | 1              | 4                 | 5              | 6.4                | 32             | 80              | Lymph nodes |
| 35         | 2              | 5                 | 6              | 6                  | 36             | 80              | Lymph nodes |
| 36         | 1              | 9                 | 10             | 4                  | 40             | 95              | Lymph nodes |
| 37         | 1              | 5                 | 5              | 7                  | 35             | 95              | Lymph nodes |
| 38         | 1              | 3                 | 5              | 7                  | 35             | 95              | Lymph nodes |
| 39         | 1              | 4                 | 5              | 7                  | 35             | 80              | Lymph nodes |
| 40         | 1              | 5                 | 5              | 6                  | 30             | 80              | Lymph nodes |
| 41         | 1              | 3                 | 5              | 10                 | 50.0           | 95              | Lung     |
| 42         | 3              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 43         | 1              | 2                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 44         | 1              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 45         | 1              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 46         | 1              | 2                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 47         | 1              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 48         | 1              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 49         | 2              | 3                 | 3              | 13.5               | 40.5           | 65              | Lung     |
| 50         | 1              | 2                 | 3              | 13.5               | 40.5           | 65              | Lung     |
sequence 3D setup MRI scan was acquired for translational patient setup correction (couch shift). For more information about the MR pulse sequences and the technical design of the MRIdian system, refer to Klüter et al. [47]. The MRI of the baseline plan was then registered via DIR to the volumetric setup MRI of the day and all target structures, OARs and the electron density of the planning CT were propagated onto the setup MRI. All contours were edited (if necessary), a tracking contour was defined and the baseline plan was calculated on the MRI (more precisely the synthetic CT) of the day, which results in the so-called predicted dose (baseline plan calculated on the anatomy of the day with updated structures). This dose distribution shows the dose of a single non-adapted fraction and is the basis to decide whether to adapt a plan or not. In case of a subsequent plan adaption, the initial predicted dose corresponds to the dose distribution prior to plan adaption. For most OARs, a time-saving and practical partial re-contouring approach was used, in which the OARs were edited only in the close surrounding of the PTV (PTV + 3.0 cm), where the highest dose gradients occur. This approach was described by Bohoudi et al. [2], while Ahunbay et al. described a similar basic concept [48]. When the decision was made to adapt the plan of the current fraction, the plan parameters and dose constraints of the baseline plan were used as a starting point for dose optimization. A treatment plan was adapted if either the target coverage or OAR constraints of the predicted plan were not fulfilled, or a combination of both. Therefore, the planning goal was always to achieve optimal target coverage while respecting all OAR constraints. Online plan adaption was performed either as re-optimization with the same objectives of the baseline plan or as full re-optimization with modified objectives and/or plan parameters. The dose distribution of the online adapted plan, calculated on the current synthetic CT (based on the MR of the day) with updated structures is referred to as re-optimized dose. All dose calculation settings for the re-optimized dose were the same as for the predicted dose (as defined in the baseline plan). After plan adaption, the dose was verified for QA using a secondary Monte Carlo code before treatment.

For tumor tracking via a 2D bSSFP cine MRI sequence, the tracking structure was propagated onto a 2D cine MRI slice and a gating ROI was created by expansion of the tracking structure. These structures were subsequently used for online beam gating. All patients in which the target volume showed a breathing-related motion were treated using a breath-hold technique (mostly deep inspiration breath hold). However, patients treated with a free breathing approach (in cases of very limited tumor motion, e.g. most prostate cases) were also treated using the automated gating function in order to ensure that the target was positioned within tolerance boundaries during treatment application.

All baseline plans were validated dosimetrically with an ionization chamber and/or diode detector array (ArcCheck-MR; Sun Nuclear Corporation, Melbourne, FL, USA) prior to the first fraction.

Extraction of DVH and plan parameters
Several dose volume histogram (DVH) parameters were extracted from the TPS for the predicted (non-adapted) and re-optimized scenarios for all fractions: the dose to 98%, 95%, 50% and 2% of the volume of the PTV (PTV D98% = near minimum dose, PTV D95%, PTV D50% = median dose, PTV D2% = near maximum dose) and the mean PTV dose (PTV Dmean). All parameters were also reported for the GTV. In prostate cases, the CTV was reported, as no GTV was defined. Furthermore, the volume of the PTV (VPTV) was extracted. Out of usually multiple, patient-specific OAR constraints prescribed in the TPS, three OAR constraints were chosen for OARs, which were closest to the PTV and as a result received the highest maximum dose values. Only OAR constraints were chosen, which were related to structures that were updated (in the PTV + 3.0 cm region; see last subsection). The individual OAR dose constraints (near maximum dose or dose-to-volume constraints) depend on the dose prescription and the individual case and were defined by a senior physician based on the applicable guidelines.

Technical plan parameters like the net beam-on time (BOT), the number of segments, the number of Monitor Units (MU) and the number of beams were read out from treatment plan documentation files (Table 2; Results).

Comparison of DVH parameters, statistical analysis and definition of dosimetric endpoints
First the OAR related DVH parameters for the predicted and re-optimized doses of each adapted fraction were compared.

Second, the same comparison was made for target volume (PTV, CTV or GTV) related DVH parameters. These parameters were systematically compared pairwise.

Table 1 (continued)
The dose prescription refers to the corresponding isodose
to quantify the DVH-based dosimetric benefit of online plan adaption for each subgroup separately. Primary dosimetric endpoints were chosen as follows: increase in GTV (all cases except prostate) or CTV (prostate cases) D98%, increase in GTV or CTV D95%, increase in GTV mean dose, reduction in OAR exposure. The GTV (or CTV) near-minimum parameters (D98% and D95%) were chosen because underdose (e.g., dose drop at the surface or cold spots) within the GTV/CTV are likely to affect the local control (LC). The GTV (or CTV in prostate cases) mean dose was chosen because there is evidence for a predictive value of this parameter in terms of improved LC in liver [49] and lung tumors [50]. Box-plots were generated to visualize the data. Therefore, due to the different dose prescriptions, data was normalized. The D₉₈% and D₉₅% dose values were normalized to the prescribed dose (PD) for non-homogenous stereotactic prescriptions (65% or 80% prescription isodose PI) or 0.95 × PD for homogenous prescriptions (95% PI). The D₅₀% and D₉₉₅ mean dose values were normalized to the PD. The D₂% was normalized to PD/PI (thus PD/0.8 for a prescription to the 80% isodose) for stereotactic prescriptions or to PD for homogenous prescriptions. Since all normalization factors depend solely on the planning aim for the PTV, these factors may differ between patients but the same factors are applied to all fractions of a single patient. The dose normalization was done to achieve comparable data for the generation of analysis figures. Statistical analysis or the calculation of percent changes of dose values is not affected by this normalization. Statistical analysis of the DVH-based parameters was performed via paired Wilcoxon signed-rank test. A significance level of α = 5% was used.

Results

Characteristics of the online adapted plans are shown in Table 2.

Figure 1 shows an example DVH of a single adaptive fraction of an abdominal lymph node case and illustrates the large potential of online ART to increase target coverage and OAR sparing with the oMRgRT technique. For example, the GTV D₉₅% improved by more than 10.0% and the duodenum D₅₀% was reduced by about one third.

Figure 2 indicates for each subgroup the change of OAR exposure when plans were adapted. The three most frequently considered OARs per region were bowel, duodenum, stomach (for liver), lung, heart, esophagus (for lung), bowel, duodenum, spinal cord (for lymph nodes), duodenum, stomach, bowel (for pancreas), and rectum, bladder, femur (for prostate). The largest median dose reduction of OARs adjacent or close to the PTV was found for the pancreas subgroup (-87.0%). This dose reduction was significant, as well as the smaller dose reduction achieved in the lymph-nodes subgroup. Small but significant median increased OAR doses were found for liver and lung and no statistically significant difference was found for prostate. All p-values and median percent changes are shown in the first row of Table 3. For a more detailed insight in the effect on individual OARs, Table 4 provides mean and median percent changes of

| Table 2 | Characteristics of the online adapted plans |
|---------|--------------------------------------------|
|         | Liver | Lung | Lymph nodes | Pancreas | Prostate |
| Adapted fractions (%) | 93.3 | 84.4 | 82.1 | 92.0 | 69.4 |
| Mean BOT (min) | 7.1 | 9.1 | 4.5 | 6.2 | 1.9 |
| Min. BOT (min) | 4.9 | 4.5 | 2.5 | 3.2 | 1.1 |
| Max. BOT (min) | 11.3 | 17.7 | 9.4 | 9.3 | 4.4 |
| Mean number of beams | 12 | 10 | 16 | 15 | 14 |
| Min. number of beams | 9 | 8 | 9 | 13 | 9 |
| Max. number of beams | 16 | 15 | 19 | 17 | 21 |
| Mean number of segments | 33 | 26 | 72 | 70 | 54 |
| Min. number of segments | 13 | 9 | 12 | 46 | 33 |
| Max. number of segments | 54 | 40 | 100 | 95 | 129 |
| Mean MU | 4269.2 | 5439.9 | 2652.2 | 3688.4 | 1139.4 |
| Min. MU | 2950.3 | 2675.2 | 444.3 | 1906.7 | 649.0 |
| Max. MU | 6776.0 | 10,612.0 | 5607.9 | 5547.1 | 2624.5 |
| Mean VₑPTV (cm³) | 38.4 | 15.2 | 65.5 | 251.1 | 114.7 |
| Min. VₑPTV (cm³) | 7.3 | 3.9 | 1.9 | 59.6 | 67.9 |
| Max. VₑPTV (cm³) | 1099 | 32.0 | 291.3 | 455.8 | 192.6 |

BOT = beam-on time, MU = number of monitor units, VₑPTV = volume of the PTV
OAR dose parameters of three most frequently considered OARs per region.

For the target volume DVH parameters, the largest changes were found for $D_{98\%}$ and $D_{95\%}$ for the PTV and GTV/CTV when comparing the re-optimized with the...
predicted doses (Fig. 3). All PTV D$_{98\%}$ and D$_{95\%}$ median dose values increased significantly across all subgroups. More importantly, the GTV/CTV D$_{98\%}$ and D$_{95\%}$ values increased significantly, except for pancreas, where no significant difference was found (see Table 3). This means that the target volume dose coverage increased significantly in most cases when adapting. The largest median increases of PTV D$_{95\%}$ were found in liver, lung and lymph nodes. The largest median increases in GTV D$_{95\%}$ were also found in the same subgroups. Although a relatively large significant increase was found for PTV D$_{95\%}$ in pancreatic cases, no significant increase was found for the pancreas GTV D$_{98\%}$ and GTV D$_{95\%}$. Despite being statistically significant, smaller median increases in PTV D$_{98\%}$, PTV D$_{95\%}$, GTV/CTV D$_{98\%}$ and GTV/CTV D$_{95\%}$ were found for prostate, compared to the liver, lung and lymph node subgroups. All $p$-values and median percent increases are shown in Table 3.

Additional target dose volume parameters are shown in Fig. 4. The near maximum doses D$_{2\%}$ did not show significant changes in most cases. Significant but small median near maximum dose reductions inside the PTV or GTV were found for PTV D$_{2\%}$ (pancreas) and GTV D$_{2\%}$ (lung). When looking at the boxplots (Fig. 4), it can be seen that a few cases of the lung, lymph node and pancreas subgroups showed predicted near maximum doses which exceeded 10% of the ideally achieved maximum dose (mostly outliers). A slight reduction of these high near maximum doses was achieved when adapting. After plan adaption, all non-outlier near-maximum values

### Table 3

$p$-values and median percent changes [p value/median change (%)] of DVH OAR and target volume parameters when comparing the re-optimized versus the predicted dose distributions

| Liver | OAR | PTV D$_{mean}$ | PTV D$_{2\%}$ | PTV D$_{95\%}$ | GTV or CTV D$_{mean}$ | GTV or CTV D$_{2\%}$ | GTV or CTV D$_{50\%}$ | GTV or CTV D$_{95\%}$ | GTV or CTV D$_{98\%}$ |
|-------|-----|----------------|---------------|---------------|-----------------------|----------------------|----------------------|----------------------|----------------------|
|       | 0.000/6.9 | 0.000/3.8 | 0.712/0.1 | 0.000/17.3 | 0.004/1.0 | 0.040/0.6 | 0.001/2.6 | 0.000/25.5 | 0.000/6.3 |
| Lung  | 0.004/5.9 | 0.006/1.0 | 0.131/−0.7 | 0.000/6.0 | 0.012/0.9 | 0.127/0.6 | 0.006/0.0 | 0.000/7.8 | 0.000/3.9 |
| Lymph nodes | 0.001/−4.5 | 0.000/3.0 | 0.757/0.0 | 0.000/9.4 | 0.000/1.4 | 0.020/1.0 | 0.003/0.9 | 0.000/15.6 | 0.000/6.8 |
| Pancreas | 0.000/−87.0 | 0.041/0.8 | 0.002/−0.9 | 0.000/5.7 | 0.454/−1.3 | 0.164/−1.4 | 0.196/−0.5 | 0.000/11.0 | 0.176/−0.8 |
| Prostate | 0.135/0.9 | 0.093/−0.2 | 0.021/0.3 | 0.000/2.8 | 0.007/0.4 | 0.185/0.2 | 0.176/−0.1 | 0.000/5.8 | 0.000/1.3 |

Significant differences are highlighted bold

*GTV for all subgroups except prostate and CTV for prostate

### Table 4

Mean and median percent changes when comparing the re-optimized versus the predicted dose distributions [mean change (%)/median change (%)] of the most frequently used OAR dose parameter for each of the three most frequently considered OARs per region

| Liver | D$_{max}$ (bowel) | D$_{max}$ (duodenum) | D$_{max}$ (stomach) |
|-------|-------------------|----------------------|---------------------|
|       | 18.2/8.5          | 35.6/50.8            | 11.2/14.0           |
| Lung  | V15$_{Gy}$ (lung left or right) | D$_{max}$ (heart) | D$_{max}$ (esophagus) |
|       | 9.0/5.9           | 18.3/0.0             | 3.6/8.2             |
| Lymph nodes | V20$_{Gy}$ (bowel) | V18$_{Gy}$ (duodenum) | D$_{max}$ (spinal canal) |
|       | −10.8/−27.8       | −43.9/−48.2          | −2.9/−4.4           |
| Pancreas | V33$_{Gy}$ (duodenum) | V33$_{Gy}$ (stomach) | V33$_{Gy}$ (bowel) |
|       | −94.8/−97.1       | −84.0/−99.1          | −83.4/−98.6         |
| Prostate | V40$_{Gy}$ (rectum) | V40$_{Gy}$ (bladder) | D$_{max}$ (femur left or right) |
|       | 6.8/0.3           | 9.3/7.4              | −0.7/−1.2           |
PTV D2% and GTV D2% exceeded the ideally achieved maximum dose by less than 10%. PTV and GTV/CTV median (D50%) and mean (Dmean) doses show an inverse behaviour. For these values, slight median increases were found in most cases, except for the pancreas subgroup, where no significant changes were found for PTV D50%, GTV D50% and GTV Dmean (Table 3).

Discussion
Liver
For the liver subgroup, the initial predicted median PTV coverage (here PTV D98% and PTV D95%) before plan adaption was worse compared to lung and prostate but was comparable to lymph nodes and pancreas. One reason might be that less complex shaped (sphere-like) targets, as small lung lesions (lung: mean VPTV = 15.2 cm³ vs. liver: mean VPTV = 38.4 cm³, see Table 2) or prostate targets, are easier to cover with default baseline plans. After plan adaption, a largely improved PTV coverage was found, which resulted in a close-to-ideal post-adaption PTV coverage, similar to that of the lung cases. With 93.3% of all fractions adapted, liver showed the highest portion of adapted plans (similar to pancreas with 92.0%). This means that the initial target volume coverage using the base plan was not ideal in almost every fraction. After plan adaption, PTV D98% was > 97.0% of the PD in all fractions. Even though the initial median PTV coverage was worse compared to the lung cases, the initial GTV coverage was similar, which means that the PTV, designed for liver cases in breath hold technique, worked very well. When comparing the normalized percent values of Fig. 3 between these two (or any other) subgroups, especially for the GTV, one has to bear in mind that all liver cases had a stereotactic prescription to the 65% isodose, but only 8/10 lung cases had the same prescription. No significant change in the PTV or GTV near-maximum dose was found, just like for most other subgroups. Regarding OAR sparing, Fig. 2 shows a more or less symmetrical distribution around zero for liver, but with a significantly increased median OAR dose. This is because OAR dose
limits were, on average, not fully reached prior to adaptation. This tendency can also be seen when looking at the exposure changes of the three most frequently considered OARs (bowel, duodenum, stomach, see Table 4), where mean and median increases in dose for all these OARs were found for liver. During the optimization process, the OAR exposure was fully exploited and brought closer to the dose limits, in order to achieve a very good target coverage without violation of OAR constraint. With a mean number of 33 segments, adapted liver plans
were simpler compared to those of lymph node, pancreas and prostate cases.

**Lung**

For lung cases, the initial PTV coverage of the predicted base plan was better compared to liver, but could still be significantly improved and resulted in a near-optimal PTV coverage after plan adaption. The initial GTV coverage was similar to that of liver, but could still be significantly improved. With 84.4% of all fractions adapted, lung showed similar adaption rates as lymph node cases. Regarding OAR sparing and change of PTV near-maximum doses, similar findings were made as for the liver subgroup. The mean PTV volume of lung cases was the smallest of all subgroups (15.2 cm³) and so was the mean number of segments (26), indicating easy-to-adapt, simple treatment plans.

**Abdominal lymph nodes**

For the abdominal lymph nodes subgroup, initial PTV coverage was not ideal but could be efficiently improved with online plan adaption, which was performed in 82.1% of fractions. As for to the liver and lung cases, a relatively large median increase (6.8%) in GTV D₉₈% was found without an increase in the near-maximum dose. The median OAR dose could be reduced significantly by – 4.5% (Table 3). A larger reduction of OAR dose was only observed in the pancreas subgroup. The lymph node treatment plans had an average number of 72 segments, which is similar to that of pancreas (70). This shows that lymph node treatment plans were usually highly modulated, similar to the pancreas plans.

**Pancreas**

Plan adaptation resulted in a significant improvement in PTV near minimum dose. Regarding the GTV coverage, no significant improvement could be made on average, when performing online plan adaption. Although the average re-optimized (and even predicted) GTV coverage was acceptable, some cases were observed where sufficient GTV coverage could not be achieved, even after plan adaption, because sparing of OARs was prioritized. This can be seen in Fig. 3, when looking at the relatively large interval between the first and third quartiles compared to those of the abdominal lymph nodes and prostate cases. The large portion of adapted fractions (92.0%) indicates the need for plan adaptation to reduce OAR doses to meet clinically acceptable OAR dose levels. OAR doses could be reduced in more than 75.0% of all OAR constraints of all adapted fractions of the pancreas cases and the median OAR dose reduction was – 87.0% (Fig. 2). The V₃₃Gy of duodenum, stomach and bowel was reduced on average by more than 80% respectively (Table 4). Without online plan adaption, OAR dose limits would have been frequently violated.

**Prostate**

For most prostate cases, the initial PTV and especially the CTV coverage were acceptable. In only a few fractions very insufficient initial target volume coverage was found (Fig. 3). For these fractions, large improvements in PTV and even CTV coverage were made when re-optimizing the plans. On average, no significant change of OAR exposure was achieved with online plan adaption. A mean of 54 segments were needed to achieve acceptable plans, which indicates plans of medium complexity. Only 69.4% of fractions were adapted.

**Comparison between tumor entities**

All subgroups clearly benefited from online plan adaption in terms of improved PTV coverage. The improved target dose varied between the different tumor entities. To estimate the absolute dose changes of the target volumes achieved by online plan adaption, it is possible to multiply the total prescribed dose of any dose prescription (Table 1) with the corresponding median percent change of any DVH parameter of interest (Table 3) and with the percentage of adapted fractions of the corresponding patient subgroup (Table 2, line 1). Obviously, this formula can only provide a rough estimate of absolute dose changes and does not consider individual patients. Based on the underlying idea of the PTV target volume concept, one would assume that the GTV/CTV coverage physically achieved during dose application is of higher prognostic value than the PTV coverage, since the sole purpose of the PTV margins is to guarantee the GTV/CTV coverage with some degree of confidence. Under this assumption it is possible to identify subgroups that might benefit more from online plan adaption than others. In the present study, the three subgroups liver, lung, and abdominal lymph nodes had the greatest benefit from online plan adaption in terms of improved GTV coverage. After plan adaption, all three subgroups showed excellent GTV coverage (D₉₈% and D₅₅%). In addition, a large portion of fractions (>82%) required re-optimization in all three subgroups, indicating that most of these fractions can be significantly improved by online plan adaption. Since small values of GTV D₉₈% and D₅₅% indicate insufficient GTV coverage, these indices can be considered the most predictive (of all DVH parameters examined) in terms of improved tumor control probability (TCP) and possibly LC when comparing non-adapted and online adapted fractions. However, it remains unclear if the significant increases in GTV near-minimum and mean doses will translate into a detectable improved LC.
In addition to the significantly improved GTV coverage in the liver, lung and abdominal lymph nodes subgroups when using plan adaption, these subgroups might also largely benefit from the breath-hold and automated beam gating capabilities of the oMRgRT system, since no internal target volume concept is needed. An internal target volume concept would increase the total irradiated volume [51], especially for these cases, where breathing-related motion of target volumes can be frequently seen. In this study, the influence of beam-gating was not investigated and no motion range assessment was made for the target volumes. That is beyond the scope of this study.

It was found for pancreas, that the plan adaption capabilities were largely used to reduce OAR doses to an acceptable level. Although the re-optimized GTV coverage was acceptable in most cases, the improvement in GTV coverage via online plan adaption was not as large as in the other subgroups, as OAR sparing was prioritized. In contrast, in the prostate subgroup, only 69.4% of all fractions were considered for re-optimization. For most of these fractions, the initial CTV coverage was quite good but could still be slightly improved when adapted. Ultimately, few fractions were found, where the initial PTV and CTV coverage was unacceptable. For these fractions, online re-optimization resulted in an excellent CTV coverage. In summary, for prostate cases, the benefit of online re-optimization was found to be not as systematic as for the liver, lung, abdominal lymph nodes and pancreas cases. In each subgroup, at least one of the primary dosimetric endpoints defined under “Methods” (significant increase in GTV/CTV near-minimum and mean dose, and significantly reduced OAR exposure) was achieved (Table 3). Except for pancreas, all other subgroups met all primary endpoints related to improved GTV/CTV dose.

To the best of our knowledge, up to now, no attempt has been made to quantify the influence of MR-guided online plan adaption on DVH-related parameters and systemically compare the results between multiple subgroups with different tumor entities typically treated on integrated MR-Linac systems. Our intent was to provide information for a more informed decision making when assigning patients to the (still very limited access) MR-Linac. Henke et al. [40] analyzed 81 online adapted fractions (20 patients) in a patient cohort of mixed oligometastatic or unresectable abdominal malignancies (hepatic lesions, adrenal metastasis, pancreatic adenocarcinoma and lymph node metastases). The overall adaption rate (83.5%) was comparable to our study, although less liver fractions (66.0%) were adapted compared to our liver subgroup (93.3%). Similar to the present study, several fractions among the pancreas cases were found, where GTV dose de-escalation was necessary due to OAR proximity of the tumor. Regnery et al. [52] prospectively compared predicted versus adapted dose distributions in 154 online adapted fractions in 21 lung tumor patients. The higher adaption rate of 93.3% compared to 84.4% in the current study can be explained with the large number of ultracentral lung tumors in the cohort of Regnery et al., where OAR violations are more likely to occur due to adjacency OARs. Regnery et al. found a large increase in the minimum biologically effective dose (BED) of the PTV and a moderate increase in the minimum BED of the GTV. We observed the same tendency when considering PTV and GTV D98% or D95%. In the same study only small increases in mean BED inside the PTV and GTV were found, which is also in accordance with our findings of PTV and GTV Dmean. El Bared et al. [35] evaluated the dosimetric benefits in 10 patients treated for unresectable pancreatic cancer on a cobalt-60, 0.35 T MRI system when performing online plan adaption and reported outcome. Although comparability to our study is limited due to a fundamental discrepancy in technical design and beam quality (tri-source cobalt-60 vs. 6 MV flattening filter free Linac), El Bared also found improved PTV coverage when performing online plan adaption. However, the influence on GTV coverage was not evaluated. Placidi et al. [37] found a similar trend of improved PTV coverage in 8 pancreatic cancer patients also treated on the cobalt-60 system and similarly reported increased CTV dose after plan adaption. The influence on GTV coverage was not evaluated. Mayinger et al. [53] analyzed online adapted treatment plans of 15 patients with liver metastases and found improved PTV coverage in cases where the target volume was in close proximity to OARs. The influence on GTV coverage was not evaluated in detail. In the present study, we did not stratify patients for adjacency of OARs, but when looking at the PTV mean and near-minimum doses, we also found a significant increase after plan adaption in liver cases. Padgett et al. [43] artificially created adapted plans for 10 patients with liver cancers on the cobalt-60 system and compared the results to the non-adapted plans and also found improved PTV and GTV coverage as well as a reduced number of OAR violations (duodenum, bowel and stomach) after plan adaption. We observed the same trend regarding target volumes and reported small mean and median dose increases for OARs like duodenum, bowel and stomach. This is no contradiction to the findings of Padgett et al. since OAR sparing was prioritized over target volume coverage in our study and no hard OAR constraints were violated during plan adaption.
Conclusions
All subgroups clearly benefited from online plan adaption in terms of improved PTV coverage. Moreover, for the liver, lung and abdominal lymph node cases, a systematic improvement in GTV coverage was found, resulting in excellent target coverage after re-optimization in most fractions. In combination with the breath-hold-based technique, these subgroups can fully exploit the potential of OMRgRT systems. In the pancreatic cancer subgroup, online plan adaption resulted in largely decreased OAR doses but the target coverage could not always be improved due to the limiting OAR constraints. While many fractions of the prostate subgroup could, in theory, also be effectively treated without plan adaption, most fractions still showed improved PTV coverage and few fractions even showed large CTV coverage improvements after online plan re-optimization.

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Authors’ contributions
LN extracted technical plan parameters, performed data analysis and drafted the manuscript. CE, JB, PT and RB performed extraction of dose-related data. GL and SC supervised the study. SC designed the study. CE, MN, VM, GL, CK, MR, CB and SC reviewed the manuscript. All authors read and approved the final manuscript.

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Not applicable.

Code availability
Not applicable.

Declarations
Ethics approval and consent to participate
This study was conducted according to the guidelines of the Declaration of Helsinki, and approved by the Ethics Committee of LMU (LMU 20-291, 13 May 2020).

Consent for publication
Not applicable.

Competing interests
SC received speaker fees/travel support from ViewRay Inc. (Oakwood Village, OH, USA). All other authors declare that they have no competing interests.

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