Methodology for ballistic blunt trauma assessment

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1. Introduction

Over the past decade, numerous studies have been undertaken to understand the human body response during blunt ballistic impact. Indeed, non-penetrating ballistic trauma can occur during the use of Less-Lethal Kinetic Energy projectiles (LLKE). A study about rigid LLKE projectile impacts on Post Mortem Human Subjects (PMHS) has been carried out (Bir et al. 2004). It leads to the development of biomechanical response corridors and the use of the injury criterion VC max to establish the probability of skeletal injury (Bir and Viano 2004). Therefore, the French Ministry of the Interior and the authors develop a methodology with a coupled experimental-numerical based approach to assess blunt trauma. Among various backing materials employed as human body substitutes, the polymer gel SEBS (styrene-ethylene-butylene-styrene) has been identified as an appropriate ballistic gelatin substitute (Mauzac et al. 2010). Although gel transparency allows direct impact analysis using high-speed camera and provides information such as the dynamical wall displacement, the volume of deformation, these data are not sufficient to establish a direct link towards blunt ballistic trauma. Hence, the authors focus their research on the use of numerical tools as finite element (FE) model. Extend information can be obtained such as, strain, strain rate and pressure. In addition, the human torso FE model called HUBByx is used in this study and has shown its biofidelic ability to replicate high-speed loading accidents (Roth et al. 2013). The robustness of numerical tools may lead to the correlation of predicted results with the experimental work and the investigation of case reports. The aim of this work is to introduce a reliable method and first results based on experimental and numerical study for ballistic trauma assessment.

2. Methods

Firstly, the impact conditions of Bir reference cases, performed on the mid-sternum of PMHS, are replicated on the SEBS gel block of 25 × 25 × 25 cm size (Bir et al. 2004). The test consists in the impact of round rigid projectile of 140 g with 37 mm in diameter at 20 m/s (projectile velocity in case reports). A challenge is to correlate numerical impact with experimental one. An incompressible hyperelastic Mooney–Rivlin material model is employed and material constants are determined using an optimization by inverse method (Rivlin 1948). The impact model is built using the commercial explicit FE code Radioss (Altair Hyperworks). 52,480 hexahedral elements represent a quarter of the gel block using planes of symmetry. Concerning the material constants identification, experimental wall displacement data are used as objectives to reach in the multi-objective optimization process using global response surface method. Secondly, the same impact condition is reproduced on the HUBByx torso model using Radioss. This complex model consists in the average representation of the human thorax/abdomen/pelvis system including the main organs: heart, lungs, kidneys, liver, spleen, the skeleton, stomach, intestines, muscles and skin.

3. Results and discussion

On the one hand, Figure 1 illustrates qualitative comparison of experimental impact ((a)-left) of 140 g projectile at 20 m/s on the gel block and numerical modeling ((a)-right). Moreover, the excellent match between experimental and numerical wall displacement (Figure 1(b)) leads the authors to establish the efficiency of the material model. The two Mooney–Rivlin parameters C 10 and C 01 are respectively equal to 0.0299 and 0.0776 MPa. Once numerical model
Mooney-Rivlin material model is highly efficient to represent experimental impact on gel at a given impact velocity. For distinct impact conditions, a more elaborate material model taking into account the strain rate dependence will be necessary. Moreover, the human FE model HUByx appears to be a satisfactory representation of human body based on replications of high-speed impact. Therefore, a direct correlation between numerical FE model data and the risk of skeletal injury is expected based on the work of Bir. However, to go further on this path, statistical approach will be imperative to find a suitable transfer function between experimental data on the gel block and the risk of blunt trauma.

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Figure 1. Experimental (left) and numerical (right) backface deformation (a) – Experimental and numerical gel wall displacement through time at 20 m/s (b).

Figure 2. Human torso model and the displacement field of skeletal system in the direction antero-posterior.

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