Cingulo-Opercular Control Network Supports Disused Motor Circuits in Standby Mode

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Abstract

Whole-brain resting-state functional MRI (rs-fMRI) during two weeks of limb constraint revealed that disused motor regions became more strongly connected to the cingulo-opercular network (CON), an executive control network that includes regions of the dorsal anterior cingulate cortex (dACC) and insula (1). Disuse-driven increases in functional connectivity (FC) were specific to the CON and somatomotor networks and did not involve any other networks, such as the salience, frontoparietal, or default mode networks. Censoring and modeling analyses showed that FC increases during casting were mediated by large, spontaneous activity pulses that appeared in the disused motor regions and CON control regions. During limb constraint, disused motor circuits appear to enter a standby mode characterized by spontaneous activity pulses and strengthened connectivity to CON executive control regions.
Significance

Many studies have examined plasticity in the primary somatosensory and motor cortex during disuse, but little is known about how disuse impacts the brain outside of primary cortical areas. We leveraged the whole-brain coverage of resting-state functional MRI (rs-fMRI) to discover that disuse drives plasticity of distant executive control regions in the cingulo-opercular network (CON). Two complementary analyses, pulse censoring and pulse addition, demonstrated that increased functional connectivity between the CON and disused motor regions was driven by large, spontaneous pulses of activity in the CON and disused motor regions. These results point to a previously unknown role for the CON in supporting motor plasticity and reveal spontaneous activity pulses as a novel mechanism for reorganizing the brain’s functional connections.

Introduction

Disuse is a powerful paradigm for inducing plasticity that has uncovered key organizing principles of the human brain (2-5). Monocular deprivation revealed that multiple afferent inputs can compete for representational territory in the primary visual cortex (2). Competition between afferents also shapes the somatomotor system, and manipulations such as peripheral nerve deafferentation, whisker trimming, and limb constraint all drive plasticity in the primary somatosensory and motor cortex (3-5). Most plasticity studies to date have used focal techniques, such as microelectrode recordings, to study local changes in brain function. As a result, little is known about how behavior and experience shape the brain-wide functional networks that support complex cognitive operations (6).
The brain is composed of networks of regions that cooperate to perform specific cognitive operations (6-9). These functional networks show synchronized spontaneous activity while the brain is at rest, a phenomenon known as resting state functional connectivity (FC) (10-12). FC can be measured non-invasively in humans using resting-state functional MRI (rs-fMRI). Whole-brain rs-fMRI has been used to parse the brain into canonical functional networks (13, 14), including visual, auditory and somatomotor networks (15, 16); ventral and dorsal attention networks (9, 17); a default mode network with roles in internally directed cognition and episodic memory (8, 12); a salience network thought to assess the homeostatic relevance of external stimuli (18); a frontoparietal control network supporting error-processing and moment-to-moment adjustments in behavior (1, 19, 20); and a cingulo-opercular control network (CON), which maintains executive control during goal-directed behavior (1, 19, 21).

A more recent advance in human neuroscience has been the recognition of individual variability in network organization (22-25). Most early rs-fMRI studies examined central tendencies in network organization using group-averaged FC measurements (11, 13, 14). Recent work has demonstrated that functional networks can be described in an individual-specific manner if sufficient rs-fMRI data are acquired, an approach termed Precision Functional Mapping (PFM) (22, 23, 26-30). PFM respects the unique functional anatomy of each person and avoids averaging together functionally distinct brain regions across individuals.

Somatomotor circuits do not function in isolation. Action selection and motor control are thought to be governed by complex interactions between the somatomotor network and control networks, including the CON (1). Here, we leveraged the whole-brain coverage of rs-fMRI and the statistical power of PFM to examine disuse-driven plasticity throughout the human brain.
Results

Disuse Caused Both Increases and Decreases in Functional Connectivity

Three adult participants ("Cast1", "Cast2" and "Cast3") were scanned at the same time every day for 42-64 consecutive days (30 minutes of rs-fMRI/day) before, during and after two weeks of dominant upper extremity casting (31). To examine disuse-driven plasticity beyond somatomotor networks, we first generated seed maps showing FC between L-SM1_{ue} and all other cortical regions before, during and after casting (Fig. 1A, S1). Prior to casting (Pre), L-SM1_{ue} was strongly connected to the remainder of the somatomotor cortex (pre- and post-central gyri), especially homotopic R-SM1_{ue}. During the cast period (Cast), L-SM1_{ue} showed a new pattern of connectivity, with strong connections to bilateral secondary somatosensory cortex (SII), dorsal anterior cingulate cortex (dACC), and pre- and post-central sulci. After casting (Post), L-SM1_{ue} FC returned to baseline. Changes in FC during casting (Cast – Pre) and recovery (Post – Cast) were examined using sets of previously published individual-specific cortical parcels (22, 31). Casting caused decreased L-SM1_{ue} connectivity with the remainder of the somatomotor cortex, as well as increased connectivity with the bilateral SII, dACC, and pre- and post-central sulci (Fig. 1B, S1). FC changes after cast removal were strongly negatively correlated with changes during casting (Cast1: spatial correlation, r = -0.56, Cast2: r = -0.95, Cast3: r = -0.32; all participants: P < 0.001), indicating that most effects reversed after cast removal (Fig. 1B, S1).

Disuse-driven Functional Connectivity Changes Were Highly Focal in Network Space

The brain’s functional network organization can be visualized using spring-embedded graphs, which treat functional connections as spring forces, positioning more strongly connected nodes closer to one another (Fig. 2A, S2). While L-SM1_{ue} FC increases were distributed in anatomical space, including regions on the medial and lateral surfaces of both hemispheres, nearly all of
these changes mapped onto a single cluster in network space, the CON (Fig. 2B, S2). The network focality of L-SM1ue FC increases was quantified by examining the distribution of the greatest FC increases (top 5%) across the canonical functional networks (Fig. 2B). In all participants, the CON showed more FC increases than expected by chance (P < 0.001 for all participants). Decreases in L-SM1ue FC were also localized in network space (Fig. 2C, S2). Most of the regions showing decreased FC with L-SM1ue during casting belonged to the somatomotor networks (ue-SMN, le-SMN, face-SMN and premotor). All participants showed more FC decreases than expected by chance in the upper-extremity somatomotor network (ue-SMN; P < 0.001 for all participants). Additionally, two participants (Cast2 and Cast3)
showed significant FC decreases in other somatomotor networks, including the lower-extremity and face somatomotor networks (le-SMN and f-SMN) and the premotor network.

Fig. 2, Disused Somatomotor Cortex (L-SM1<sub>ue</sub>) Functional Connectivity (FC) Changes in Network Space. (A) Map of canonical functional networks in an example participant (Cast2; remaining participants, Fig. S1). Left: Networks shown in anatomical space (inflated cortical surfaces). Middle: Same map as Top, shown in network space (spring-embedded graphs based on Pre scans). Right: Network color key: m-Vis: medial visual; l-Vis: lateral visual; Aud: auditory; f-SMN: face somatomotor; ue-SMN: upper-extremity somatomotor; le-SMN: lower-extremity somatomotor; CON: cingulo-opercular; FPN: fronto-parietal; Sal: salience; DAN: dorsal attention; VAN: ventral attention; PMN: parietal memory; CAN: context association; DMN: default mode. (B) Left: Subtraction maps showing disuse-driven decreases in functional connectivity (FC) with left somatomotor cortex (L-SM1<sub>ue</sub>) in anatomical space. Middle: Same map as Top, shown in network space. Right: Distribution of top 5% FC decreases across all networks. **P < 0.01; ***P < 0.001; FDR < 0.05. (C) Subtraction maps showing disuse-driven increases in FC with L-SM1<sub>ue</sub> in anatomical (Left) and network space (Middle). Right: Distribution of top 5% FC increases across all networks.
Plasticity Was Restricted to the Somatomotor and Cingulo-opercular Networks

The analyses presented thus far focus on changes in connectivity between L-SM1ue and the remainder of the cerebral cortex. To examine whole-brain patterns of FC changes induced by casting, we extracted rs-fMRI signals from individual-specific cortical, subcortical and cerebellar parcels (Cast1: 744 parcels, Cast2: 733; Cast3: 761) and examined FC changes in all possible pairwise connections (Fig. S3). We displayed the 50 largest changes in FC (25 greatest increases and 25 greatest decreases) in anatomical space (Fig. 3A, S3). Disuse-driven FC changes involved L-SM1ue more than expected by chance (Cast1: 9/50 connections, $P = 0.018$; Cast2: 37/50, $P < 0.001$; Cast3: 39/50, $P < 0.001$). Figure 3B shows the total

Fig. 3. Whole-brain Analyses of Disuse-driven Functional Connectivity (FC) Changes. (A) Changes in functional connectivity (FC) were computed for all pairs of cortical, subcortical and cerebellar parcels (mean Cast FC – mean Pre FC). The 50 most altered functional connections (top 25 increases, top 25 decreases) are shown for an example participant (Cast2; all participants, Fig. S3). (B) For each vertex/voxel, the magnitude of whole-brain FC change was computed as the sum of squared FC changes between that vertex and every other gray-matter vertex/voxel. Shown for an example participant (Cast2; all participants shown in Fig. S4).
magnitude of whole-brain FC change for each vertex/voxel. The total magnitude of whole-brain FC change was significantly greater in L-SM1_{ue} than in the remainder of the brain (Fig. 3B, S3; Cast1: P = 0.021; Cast2: P < 0.001; Cast3: P = 0.005).

**Increased Connectivity with the CON Depended on a Recent History of Disuse**

To distinguish between increases in connectivity due to wearing a cast during MRI scans (i.e., an altered behavioral state) and increases in connectivity due to a history of having been casted (i.e., disuse-driven plasticity), we conducted a control experiment in which participants wore casts during 30-minute scans but were not casted during their daily lives. In both cases, we compared FC between L-SM1_{ue} and the left dorsal anterior cingulate cortex (L-dACC; Fig. S4A), a key node of the CON, in cast and no-cast conditions. As suggested by the whole-brain network analyses (Fig. 2B), FC between L-SM1_{ue} and L-dACC was significantly increased during the cast period (Fig. S4B). When participants wore casts during scans, but were not casted during their daily lives, no changes in FC were observed (Fig. S4C). This control experiment indicated that increased FC between the disused motor circuitry and the CON depended on participants’ recent history of disuse, not their current state of casting.

**Network-Specific Connectivity Changes Reflect Spontaneous Activity Pulses**

Increases in FC with L-SM1_{ue} showed a similar anatomical distribution to the spontaneous activity pulses we described previously (31) (Fig. S5A-B). Additionally, FC between L-SM1_{ue} and the CON was highly correlated with the number of pulses detected in L-SM1_{ue} during each scan (Fig. S5C; Cast1: r=0.74, Cast2: r=0.57, Cast3: r=0.73; all participants: P<0.001). These observations led us to suspect that FC between L-SM1_{ue} and the CON was increased during the cast period because both regions showed synchronized spontaneous activity pulses.
To test if spontaneous activity pulses could explain observed increases in FC, we implemented a pulse censoring strategy, in which frames surrounding each detected pulse (13.2 s before – 17.6 s after each pulse peak) were excluded from FC calculations (Fig. 4A). This approach is similar to the censoring strategy commonly used to correct the effects of head-motion on FC (32). Censoring pulses partially reduced the FC changes observed during casting (Fig. 4B; Cast1: -55%, P = 0.14; Cast2: -28%, P = 0.02; Cast3: -21%, P = 0.04; one-tailed t-test).

Additionally, the spatial pattern of FC changes caused by pulse censoring (Censored – Uncensored; Fig. 4C, S6) was negatively correlated with FC changes during casting (Cast1: r = -0.35, Cast2: r = -0.90, Cast3: r = -0.33; all participants: P < 0.001).

Censoring pulses did not entirely eliminate the effect of casting on FC. The residual effect of casting after pulse censoring was negatively spatially correlated with the effects of pulse censoring (Fig. S6; Cast1: spatial correlation, r = -0.23, Cast2: r = -0.76, Cast3: r = -0.18; all participants: P < 0.001), suggesting that the residual effect may have been driven by...
additional pulses that were too small to distinguish from ongoing spontaneous activity fluctuation. Pulses showed a wide distribution of magnitudes (Fig. 5A; range: 0.4 – 1.2% rs-fMRI signal change). Because pulses were detected using a threshold-based approach (31), pulses smaller than 0.4% fMRI signal change could not be detected and censored. To test if smaller pulses that escaped detection could explain the residual increased FC between L-SM1ue and L-dACC after pulse censoring, we simulated a full distribution of pulse magnitudes by adding the mean pulse time series from L-SM1ue and L-dACC to the baseline rs-fMRI signals recorded from these regions prior to casting (Fig. 5B). Simulated pulse magnitudes were drawn from a log-normal distribution, fit to the magnitude distribution of detected pulses using a least-squares approach (Fig. 5A; see S7 for triangular and exponential distributions). Adding simulated pulses caused FC increases with a similar effect size (Cast1: Δr = +0.07, P = 0.013; Cast2: +0.40, P < 0.001; Cast3: +0.19, P < 0.001) to the FC increases observed during
casting (Fig. 5C). Applying the same pulse censoring strategy described above to the simulated pulses partially reduced the increases in FC (Fig. 5C; Cast1: -79%, Cast2: -58%, Cast3: -69%; all participants: P < 0.001), similar to the effect of pulse censoring on the actual data (Fig. 4B). Adding simulated pulses to all brain regions, using mean pulse time series specific to each region, recreated the anatomical distribution of FC changes observed during casting (Fig. 5D, S8; Cast1: r = 0.44, Cast2: r = 0.95, Cast3: r = 0.64; all participants: P < 0.001). Thus, pulse with a full distribution of magnitudes could account for observed FC changes during casting and the partial reversal of FC changes after pulse censoring.

We also utilized the pulse censoring and pulse addition analyses to test if pulses could explain observed decreases in FC within the somatomotor system. Pulse censoring did not significantly reverse the decrease in FC between L-SM1_\text{ue} and R-SM1_\text{ue} observed during the cast period (Fig. S9). Adding simulated pulses to baseline time series decreased FC between L-SM1_\text{ue} and R-SM1_\text{ue}, but this effect was much smaller than that observed during casting (Fig. S9).

**Discussion**

**Disuse Drives Plasticity of Functional Networks**

Daily 30-minute scans of rs-fMRI before, during, and after casting revealed that disuse not only causes plasticity within the primary motor cortex (4, 31), but also increased functional connectivity between disused circuits and executive control regions in the CON. These increases in FC would have been difficult to observe using the focal recording techniques traditionally employed to study plasticity. Thus, understanding the total impact of disuse on brain function requires consideration of plasticity at multiple spatial scales.
The high degree of network specificity seen in disuse-driven plasticity is a powerful demonstration of the validity of individual-specific rs-fMRI network parcellations. It could have been the case that casting produced a complex pattern of FC changes involving many brain systems. Instead, we found that virtually all of the regions showing increased connectivity with the disused motor cortex belonged to a single network, the CON. Thus, large-scale functional networks seem to be a fundamental unit of brain organization, important not only for understanding patterns of activation during cognitive processes, but also for understanding whole-brain patterns of plasticity.

**Spontaneous Activity Pulses Alter Functional Connectivity**

The network-specific increases in FC between the disused L-SM1ue and the CON likely reflect the emergence of synchronized spontaneous activity pulses in these regions during casting. FC is a measurement of the temporal correlation of spontaneous activity between brain regions. Two complementary analyses (pulse censoring and pulse addition) suggested that pulses contributed to increases in measured FC between disused motor regions and the CON. Many studies have reported increased FC in neuropsychiatric conditions, e.g., Parkinson's disease (33) and Major Depressive Disorder (34). Perhaps some previously reported FC increases could reflect spontaneous activity pulses, similar to those caused by limb disuse. Going forward, spontaneous activity pulses, and the network-specific FC changes they produce, could serve as a biCast3ker of recent disuse and states of heightened plasticity (35).

Decreases in connectivity within the somatomotor system were not fully explained by spontaneous activity pulses. Although the pulse addition analyses showed that spontaneous activity pulses could contribute to decreases in connectivity observed during casting, both the pulse censoring and pulse addition analyses suggested that at least part of the observed
decrease in connectivity occurred independently of pulses. Loss of typical co-activation of L-SM1\textsubscript{ue} and R-SM1\textsubscript{ue} during daily behavior (31) likely contributed to cast-driven connectivity decreases, consistent with the widely held hypothesis that FC is maintained by a Hebbian-like mechanism that depends on co-activation of brain regions during behavior (19, 36-39).

**Disuse Impacts Cingulo-opercular Network (CON) Important for Executive Control**

The importance of control systems in the human brain has been recognized for several decades (7), but our understanding of these systems has changed dramatically over time and continues to evolve (40). Disentangling the roles of two networks mediating executive control, the cingulo-opercular and frontoparietal networks, has relied largely on complex task designs such as task-switching (21) and slow-reveal paradigms (41). Here, we have demonstrated that a new approach, whole-brain precision functional mapping combined with anatomically specific disuse paradigms, can shed new light on the network interactions that support human cognition and behavior. Although the brain contains several suspected control networks beyond the CON, such as the frontoparietal (FPN), dorsal attention (DAN), ventral attention (VAN) and salience (SAL) networks, disused motor regions showed increased FC only with the CON. The CON is thought to initiate goal-directed behaviors and maintain executive control settings in relation to task objectives (1, 19). The increased FC between disused L-SM1\textsubscript{ue} and the CON during casting suggests either 1) circuits within the CON were also disused during casting, 2) the CON helps to maintain disused motor circuitry, or 3) spontaneous activity pulses can spread along functional connections to neighboring brain regions in network space.

Spontaneous activity pulses may have emerged in the CON because its use was also reduced during casting. We previously suggested that spontaneous activity pulses found in motor regions may have been caused by disuse-driven changes in local inhibitory physiology (31,
The CON is generally thought to represent task sets, abstract parameters and motor programs governing goal-driven behaviors (1, 19). Task sets can be applied to multiple motor effectors (e.g., right hand, left index finger, etc.), so it would be reasonable to think that casting one extremity would not cause disuse of the CON. However, at least two sets of circuits within the CON may have been disused during casting: circuits that represent bimanual behaviors and circuits that convey task sets to effector-specific downstream regions (e.g., L-SM1ue).

During casting, many of the task sets previously used to control the dominant upper extremity (e.g., inserting a key into a lock) could have been used to control the non-dominant extremity. However, task sets requiring bimanual coordination (e.g., fastening a belt) could not be applied to an alternative set of motor effectors and may have become disused. Another set of CON circuits that may have been disused are the circuits that convey task set information to effector-specific brain regions. The CON contains both somatotopically organized regions (e.g., SMA, SII) and non-somatotopic regions (e.g., anterior insula). Recent work shows that the SMA and SII, as well as regions of the basal ganglia, may act as hubs that connect the rest of the CON to the somatomotor network (27, 43). Such circuits could potentially undergo disuse during casting of one extremity.

An alternative possibility is that inputs from the CON to L-SM1ue served a homeostatic function during disuse, helping to maintain motor circuits that are typically maintained through active use. We previously suggested that spontaneous activity pulses may help to maintain the organization of disused brain circuits (31). Perhaps pulses are triggered by the CON, which is the system typically responsible for initiating activation of the somatomotor network (1).

Spontaneous activity pulses may also have originated in the disused somatomotor circuits and spread along functional connections to brain regions that were not affected by casting. The
CON is immediately adjacent to the somatomotor network in network space (Fig. 2A). Previous work in mice found that spontaneous activity bursts in somatosensory cortex, caused by local pharmacogenetic suppression of inhibitory interneurons, spread to other functionally connected regions not targeted by the experimental manipulation (44). An interesting question for future research is whether the CON would show spontaneous activity pulses following disuse of brain systems other than the somatomotor network, such as networks supporting visual and auditory processing, spatial navigation, or social cognition.

Two Complementary Mechanisms for Functional Network Plasticity

Extensive whole-brain imaging before, during and after casting revealed that disuse-driven spontaneous activity pulses occur not only in primary motor and somatosensory areas, but also in higher-order brain regions responsible for executive control over behavior. The emergence of spontaneous activity pulses during casting produced increases in FC that were highly focal in network space, specifically occurring between disused motor regions and the CON. Decreases in connectivity between disused motor circuits and the remainder of the somatomotor system, however, were not explained by spontaneous activity pulses. Thus, disuse may drive network plasticity through two complementary mechanisms. Decreased coactivation of brain regions during disuse might drive Hebbian-like disconnection between disused and still-active somatomotor circuits. Spontaneous activity pulses, which contributed to increased connectivity with the CON, may help preserve disused circuits for future reintegration and use. Together, these two network plasticity mechanisms—Hebbian-like and pulse-mediated—may represent a network-focal “stand-by mode” that allows the brain to isolate disused circuits while simultaneously protecting them from premature functional degradation.
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Author Contributions:
D.J.N., T.O.L., C.R.H., A.Z.S., and N.U.F.D. designed the study. D.J.N., C.R.H., J.M.H., M.O., and N.U.F.D. collected the data. D.J.N. and E.M.G. analyzed the data. D.J.N., E.M.G., T.O.L., N.A.S., D.F.M., S.J.G., A.Z., A.N.N., B.A., A.R.C., B.P.K., D.J.G., M.E.R., S.E.P., A.Z.S., and N.U.F.D. interpreted the results. D.J.N. and N.U.F.D. wrote the manuscript with input from all other authors.

Declaration of interests:
The authors declare the following competing financial interest: N.U.F.D. is co-founder of NOUS Imaging.
METHODS

Human Participants

Participants were three healthy, adult volunteers. Details are described in Newbold et al. (31).

Experimental Intervention

We constrained the dominant upper extremity for two weeks by fitting each participant with a fiberglass cast. Casts extended from just below the shoulder to past the fingertips. Details are described in Newbold et al. (31).

MRI Acquisition

Participants were scanned every day of the experiment for 42-64 consecutive days. We collected 30 minutes of resting-state functional MRI (rs-fMRI) data every day of the experiment, as well as also task fMRI and T1- and T2-weighted structural scans. Acquisition parameters and procedures are detailed in Newbold et al. (31).

MR Image Processing

Preprocessing of structural and functional images, denoising of resting-state fMRI data, and cortical surface projection were performed previously (31). Fully processed data are available in the Derivatives folder of the Cast-Induced Plasticity dataset on OpenNeuro (www.openneuro.org/datasets/ds002766).

ROI Selection

The region of the left primary somatomotor cortex controlling the casted upper extremity (L-SM1ue) was located individually in each participant using task fMRI. Details of the task analysis and region of interest (ROI) selection are described in Newbold et al. (31). The L-SM1ue ROI was used here to generate seed maps (Fig. 1, S1), to analyze spatial specificity of whole-brain functional connectivity changes (Fig. 3B, S3) and to measure FC between L-SM1ue and the dorsal anterior cingulate cortex (dACC) for the removable cast control experiment (Fig. S4), the pulse censoring analysis (Fig. 4) and the pulse addition analysis (Fig. 5, S7).
Individual-specific sets of parcels spanning the entire cerebral cortex were previously generated for each participant using a functional connectivity gradient-based approach, and each parcel was assigned to one of 17 canonical functional networks using a graph theory-based community detection algorithm (22, 31). Cortical parcels were used here to display functional connectivity changes in anatomical (Fig. 1-2, 5, S1-S2, S4-S6) and network space (Fig. 2, S2). We also generated a set of subcortical and cerebellar parcels by assigning each voxel to the functional network with which it showed the strongest functional connectivity and then grouping adjacent voxels with matching network assignments into parcels. Sets of cortical, subcortical and cerebellar parcels were used to examine changes in FC between all pairs of brain regions (Fig. 3, S2).

A subset of parcels corresponding to the left primary somatomotor cortex (L-SM1_{ue}) was previously generated by selecting all left-hemisphere parcels assigned to the upper-extremity somatomotor network, excluding any parcels that fell outside of the pre- and post-central gyri (31). Functional connections between L-SM1_{ue} parcels and all other parcels were averaged to generate parcel-wise seed maps (Fig. 1-2, 5, S1-S2, S4-S6) and to quantify the spatial specificity of FC changes between all cortical, subcortical and cerebellar parcels (Fig. 3, S3).

Individual-specific ROIs in the left dorsal anterior cingulate cortex (L-dACC) were selected using pulse analysis of variance (ANOVA) maps, which were previously generated for each participant (31). ROIs were selected within a large anatomical region, automatically labeled by FreeSurfer (union of caudal anterior cingulate gyrus, posterior cingulate gyrus, and superior frontal gyrus). We first located the vertex showing the maximum ANOVA F-statistic and then iteratively expanded the ROI by selecting neighboring vertices in descending order of F-statistic, until the ROI included 100 vertices. The L-dACC ROI was used to measure FC between L-SM1_{ue} and the L-dACC for pulse censoring (Fig. 4) and pulse addition analyses (Fig. 5, S7).
**Functional Connectivity Measurement**

Mean rs-fMRI time series were extracted from the L-SM1<sub>ue</sub> ROI and each cortical, subcortical and cerebellar parcel by averaging the time series of all vertices/voxels within the ROI/parcel. Vertex-wise functional connectivity (FC) seed maps were generated for each session by computing a Pearson correlation between the mean rs-fMRI time series from the L-SM1<sub>ue</sub> ROI and the time series from every vertex. Frames with high head motion, identified previously (31), were excluded from FC calculations. Vertex-wise seed maps were averaged across sessions before, during and after casting (Pre, Cast, Post; Fig. 1, S1).

FC between all pairs of cortical, subcortical and cerebellar parcels was measured as pairwise correlations of all mean rs-fMRI time series, excluding high-motion frames, producing a correlation matrix for each session. Correlation matrices were averaged over Pre, Cast and Post period. FC changes during casting and recovery were computed as the differences between correlation matrices (casting = Cast – Pre; recovery = Post – Cast). Full Cast – Pre differences matrices are shown in Figure S3. Parcel-wise difference seed maps showing changes in L-SM1<sub>ue</sub> FC during casting and recovery (Fig. 1-2, S1-S2) were computed by averaging together columns of the difference matrices corresponding to the L-SM1<sub>ue</sub> parcels (see ROI selection, above).

**Spring Embedding**

Cortical parcels were displayed in network space using force-directed (“spring-embedded”) graphs(45), generated with Gephi (https://gephi.org/). Graph weights were taken from parcel-wise correlation matrices averaged across all sessions prior to casting (Pre). Graphs were thresholded to include only the top 0.2% of pairwise functional connections. We initially examined graphs using an edge threshold of 0.1%, but several parcels with large FC changes were disconnected from the main graph. Thus, we selected the 0.2% connection threshold to display all key findings (Fig. 2, S2).
To test which functional networks showed large changes in FC with L-SM1\textsubscript{ue} during casting, parcel-wise L-SM1\textsubscript{ue} seed maps were compared to individual-specific network maps. Parcel-wise L-SM1\textsubscript{ue} difference seed maps (Cast – Pre) were thresholded to contain the top 5% of parcels showing FC increases/decreases. FC increases (Cast > Pre) and decreases (Cast < Pre) were examined separately. The number of supra-threshold parcels in each cortical network is shown in Figure 2. Alternative thresholds (top 1%, 10% and 20%) all yielded similar results. Networks containing a greater number of FC increases/decreases than expected by chance were identified by comparing the number of supra-threshold parcels found using each participant’s true network map to the number of parcels found using spatially permuted network maps (see Statistical analyses, below).

The spatial specificity of whole-brain plasticity was examined by comparing changes in FC between all cortical, subcortical and cerebellar parcels to individual-specific functional network maps. We examined the top 50 changes in FC (25 greatest increases and 25 greatest decreases). A change in FC between two parcels was counted as involving L-SM1\textsubscript{ue} if either of the two parcels was an L-SM1\textsubscript{ue} parcel. The number L-SM1\textsubscript{ue} changes found using each participant’s true network map was compared to the number of L-SM1\textsubscript{ue} changes found using spatially permuted network maps (see Statistical analyses, below).

To examine whole-brain FC changes at a finer spatial resolution, we examined differences in FC between all cortical, subcortical and cerebellar vertices/voxels. We computed the magnitude of whole-brain FC change between each vertex/voxel as the sum of squared FC changes between that vertex/voxel and every other gray-matter vertex/voxel (Fig. 3, S3). We tested if whole-brain FC change was higher in L-SM1\textsubscript{ue} than in the rest of the brain by comparing the mean magnitude of whole-brain FC change inside of each participant’s true L-SM1\textsubscript{ue} ROI to the mean magnitude of whole-brain FC change inside of spatially rotated ROIs (see Statistical analyses, below).
Spatial and Temporal Comparisons of Pulses and FC Changes

To generate a parcel-wise map of spontaneous activity pulses, we extracted rs-fMRI time series from every cortical, subcortical and cerebellar parcel surrounding each detected pulse (13.2 seconds before to 17.6 seconds after each pulse peak). Pulse peaks were detected previously (31). We then performed an ANOVA on the extracted time series (Fig. S5B). The spatial distribution of ANOVA F-statistics was compared to the spatial distribution of L-SM1\textsubscript{ue} FC changes using a Pearson correlation across parcels.

We also compared the number of pulses detected during each rs-fMRI scan (31) to the FC measured between L-SM1\textsubscript{ue} and L-dACC (Fig. S4C), using a Pearson correlation.

Pulse Censoring Analyses

To assess the contribution of large, detectable spontaneous activity pulses (>0.4% rs-fMRI signal change) to FC changes observed during casting, frames surrounding each pulse (13.2 seconds before to 17.6 seconds after each pulse peak) were excluded from FC calculations. Pulse detection criteria were identical to those used previously (31). We plotted FC measured between L-SM1\textsubscript{ue} and L-dACC during each session before casting (Pre), during casting (Cast) and during casting with pulses excluded (Cens; Fig. 4B). We compared Cast vs. Pre FC measurements and Cens vs. Cast FC measurements using t-tests (see Statistical analyses, below). We also generated difference seed maps showing FC changes between L-SM1\textsubscript{ue} and all cortical parcels due to censoring (Cens – Cast; Fig. 4C, S6).

Pulse Addition Analyses

To assess the contribution to FC changes of pulses with a hypothetical full magnitude distribution, including pulses that were too small (<0.4% rs-fMRI signal change) to distinguish from ongoing spontaneous activity fluctuations, we created simulated rs-fMRI time series containing a full distribution of pulses. We first generated a histogram showing the magnitude distribution of detected pulses. Magnitudes were grouped into bins with a width of 0.5%-signal-change. We then fit a log-normal distribution to the observed pulse magnitudes using a least-squares approach (Fig. 5A). This provided an estimate of the full pulse magnitude distribution, including pulses that were too small to detect.
then added the mean pulse time series to the baseline (Pre) rs-fMRI time series, drawing pulse magnitudes from the full log-normal distribution (example shown in Fig. 5B). The number of pulses added was selected so that the number of large pulses (>0.4% signal change) would match the number of pulses detected in each participant in an average Cast scan. We then computed FC of the baseline time series (Pre) and the time series with added pulses (Sim; Fig. 5C). Finally, we applied the same pulse censoring strategy described above to the simulated time series and computed FC after censoring (Cens; Fig. 5C). Because pulse magnitudes were drawn from a full log-normal distribution, only a portion of the added pulses were detected and censored. We compared Sim vs. Pre FC measurements and Cens vs. Sim FC measurements using t-tests (see Statistical analyses, below). The simulation and censoring procedures were repeated using triangular and exponential magnitude distributions (Fig. S7). We also generated difference seed maps showing FC changes between L-SM1	extsubscript{ue} and all cortical parcels due to pulse simulation (Sim – Pre; Fig. 5D, S8).

**Statistical Analyses**

All statistical tests were performed identically for each participant. Whenever appropriate, we used simple parametric statistical tests:

- Spatial similarity between anatomical maps was tested using a Pearson correlation across parcels (Cast1: d.f. = 566; Cast2: 578; Cast3: 624). Spatial correlations were computed between the following maps:
  - FC changes during casting (Cast – Pre) vs. FC changes during recovery (Post – Cast; Fig. 1B)
  - FC changes during casting (Cast – Pre) vs. pulse ANOVA (F-statistic; Fig. S5)
  - FC changes during casting (Cast – Pre) vs. FC changes due to pulse censoring (Cens – Cast; Fig. 4C, S6)
  - FC changes due to pulse censoring (Cens – Cast) vs. residual FC changes after pulse censoring (Cens – Pre; Fig. S6)
FC changes during casting (Cast – Pre) vs. FC changes due to simulated pulses (Sim – Pre; Fig. 5D, S8)

- The number of pulses detected during each scan was compared to the FC measured between L-SM1\textsubscript{ue} and L-dACC using a Pearson correlation (Cast1: d.f. = 45; Cast2: 61; Cast3: 40; Fig. S5C).

- FC between L-SM1\textsubscript{ue} and L-dACC measured during each session of the cast period (Cast1: n = 13 sessions; Cast2: 13; Cast3: 14) was compared to FC during each session of the pre period (Cast1: n = 10; Cast2: 12; Cast3: 14) using a two-sided, unpaired t-test (Cast1: d.f. = 21, Cast2: 23, Cast3: 26; Fig. S5B).

- FC between L-SM1\textsubscript{ue} and L-dACC measured using the full time series (motion-censored only) of each session of the cast period (Cast1: n = 13 sessions; Cast2: 13; Cast3: 14) was compared to FC measurements of the same sessions excluding pulses (motion- and pulse-censored) using a one-sided, paired t-test (Cast1: d.f. = 24, Cast2: 24, Cast3: 26; Fig. 4B).

- FC between L-SM1\textsubscript{ue} and L-dACC measured during each session of the pre period (Pre; Cast1: n = 10; Cast2: 12; Cast3: 14) was compared to FC measurements of the same sessions after adding simulated pulses (Sim) using a two-sided, paired t-test (Cast1: d.f. = 18, Cast2: 22, Cast3: 26; Fig. 5C).

- FC between L-SM1\textsubscript{ue} and L-dACC measured using the full time simulated series (Sim; motion-censored only; Cast1: n = 10; Cast2: 12; Cast3: 14) was compared to FC measurements of the same sessions excluding pulses (motion- and pulse-censored) using a two-sided, paired t-test (Cast1: d.f. = 18, Cast2: 22, Cast3: 26; Fig. 5C).

When parametric statistical tests were not appropriate to test a specific hypothesis, we tested results against a null distribution generated via permutation resampling. In each case, our null hypothesis was that observed effects had no spatial relationship to ROIs/functional networks and any overlap occurred by chance. For vertex-wise ROIs, we modeled the null hypothesis by rotating the ROI around the cortical surface 1,000 times (46, 47). For functional networks, we modeled the null hypothesis by
permuting the network assignments of parcels 1,000 times. Each permuted ROI/network map was used exactly as the actual map in order to compute a null distribution for the value of interest. The P-value reported for each test represents the two-sided probability that a value in the null distribution has a greater magnitude than the observed value. Permutation resampling was used to generate null distributions for the following values:

- Overlap of each functional network with increases in L-SM1ue FC during casting (Cast > Pre; number of parcels in top 5%; Fig. 2B)
- Overlap of each functional network with decreases in L-SM1ue FC during casting (Cast > Pre; number of parcels in top 5%; Fig. 2C)
- Overlap of L-SM1ue parcels with the 50 largest changes in FC between all pairs of cortical, subcortical and cerebellar parcels (Fig. 3A, Fig. S3)
- Magnitude of whole-brain FC change in the L-SM1ue ROI (Fig. 3B, S3)

Since we tested the overlap of L-SM1ue FC increases/decreases with 17 different functional networks, a Benjamini-Hochberg procedure was applied to correct for multiple comparisons, maintaining false discovery rates < 0.05. Each of the three participants constituted a separate replication of the experiment, rather than multiple comparisons, so no correction was necessary for tests repeated in each participant.

**Data Visualization**

Regions of interest and whole-brain pulse maps were shown on cortical surfaces generated by FreeSurfer (48) and Human Connectome Project (HCP) Workbench software packages (49). These images were rendered using HCP Workbench (49). Figures showing the greatest differences in functional connectivity across the entire brain in inflated anatomical space (Fig. 3, S3) were rendered using Blender, a free and open-source 3D modeling software package (www.blender.org). To make the large number of changed connections included in these images visually compact, connections following
similar spatial trajectories were drawn toward each other using a previously published mean-shift edge
bundling algorithm (50). All other figures were produced using Matlab (www.mathworks.com).

Data Availability
This study used our previously published dataset (31), available on the OpenNeuro database
(www.openneuro.org/datasets/ds002766).

Code Availability
All code needed to reproduce our analyses is available on Gitlab
(https://gitlab.com/DosenbachGreene/cast-whole-brain).
Fig. S1. Functional Connectivity (FC) Changes Involving the Disused Somatomotor Cortex (L-SM1\textsubscript{ue}) in Anatomical Space (All Participants). (A) Seed maps showing FC between L-SM1\textsubscript{ue} and the remainder of the cerebral cortex in Cast1 (top) and Cast3 (bottom). Seed maps were averaged across sessions before, during and after casting (Pre, Cast, Post). (B) Subtraction maps showing changes in FC during casting (Cast – Pre) and recovery (Post – Cast). Differences are shown on sets of 506 (Cast1) and 626 (Cast3) individual-specific cortical parcels. For Cast1 and Cast2, these parcels were previously generated and published (Gordon, 2017). We applied identical methods to generate a set of parcels for Cast3.
**Fig. S2.** Functional Connectivity (FC) Changes Involving the Disused Somatomotor Cortex (L-SM1ue) in Anatomical and Network Space in Cast1 and Cast3. (A) Maps of 17 canonical functional networks in Cast1 (top) and Cast3 (bottom). Networks are shown in anatomical space (inflated cortical surfaces) and network space (spring-embedded graphs based on Pre scans). See Figure 2 for network color key. (B) Subtraction maps showing disuse-driven decreases in functional connectivity (FC) with left somatomotor cortex (L-SM1ue) in anatomical space and network space. (C) Subtraction maps showing disuse-driven increases in FC with L-SM1ue in anatomical and network space.
Fig. S3. Whole-brain Patterns of Disuse-driven Plasticity. (A) Matrices showing changes in functional connectivity (FC) between all pairs of individual specific cortical, subcortical and cerebellar parcels during casting (Cast1: 744 parcels, Cast2: 733; Cast3: 761). (B) 50 largest changes in FC shown in anatomical space. (C) Magnitude of whole-brain FC change, computed as the sum of squared FC changes between each vertex/voxel and every other gray-matter vertex/voxel.
Fig. S4. Connectivity between Disused Somatomotor Cortex and Cingulo-opercular Network during Disuse and Temporary Casting. (A) Example regions of interest (ROIs) in the left primary somatomotor cortex (L-SM1ue) and the left dorsal anterior cingulate cortex (L-dACC). (B) Functional connectivity (FC) measured between L-SM1ue and L-dACC before (Pre), during (Cast) and after casting (Post). Two participants (Cast2 and Cast3) show a significant increase in FC during the cast period +P < 0.1, *P < 0.05, ***P < 0.001. (C) FC measured between L-SM1ue and L-dACC during both conditions of the control experiment: without casting (Off) and with temporary casts during scans (On). No changes in FC were observed.
**Fig. S5.** Relationship of Spontaneous Activity Pulses to Functional Connectivity (FC) Changes. (A) Increases in FC with the disused somatomotor cortex (L-SM1ue) during casting, repeated from Figure 2B for reference. (B) Analysis of variance (ANOVA) showing regions with spontaneous activity pulses. ANOVA F-statistic was correlated with FC change in each parcel (Cast1: $r = 0.16$, $P < 0.001$; Cast2: $r = 0.29$, $P < 0.001$; Cast3: $r = 0.06$, $P = 0.12$). (C) Relationship of FC between L-SM1ue and the dorsal anterior cingulate cortex (dACC; cingulo-opercular network (CON)) vs. the number of pulses detected. Each dot represents one 30-minute scan. Colored dots represent scans during the cast period. For all participants, FC between L-SM1ue and dACC was significantly correlated with the number of pulses detected (Cast1: $r=0.74$, $P<0.001$; Cast2: $r=0.57$, $P<0.001$; Cast3: $r=0.73$, $P<0.001$).
**Fig. S6.** Functional Connectivity (FC) Changes Explained by Spontaneous Activity Pulses. (A) Subtraction map showing changes in L-SM1ue FC due to pulse censoring. The spatial pattern of FC changes due to pulse censoring was negatively correlated with FC changes during casting (Cast1: \( r = -0.35, P < 0.001 \); Cast2: \( r = -0.90, P < 0.001 \); Cast3: \( r = -0.33, P < 0.001 \)). (B) Subtraction map showing residual FC changes during casting after pulse censoring. The spatial pattern of residual FC changes was negatively correlated with the effect of pulse censoring (Cast1: spatial correlation, \( r = -0.23, P < 0.001 \); Cast2: \( r = -0.76, P < 0.001 \); Cast3: \( r = -0.18, P < 0.001 \)).
**Fig. S7.** Alternative Distributions for Pulse Magnitudes. (A) Exponential distribution. *Left:* Histogram of pulse magnitudes (peak fMRI signal), pooled across all participants. An exponential distribution (black line) was fit to the data using a least-squares approach. *Right:* Adding simulated pulses, with magnitudes drawn from the exponential distribution, increased FC between L-SM1_ue and L-dACC. Censoring simulated pulses partially reduced FC increases. *P*<0.05, **P*<0.01, ***P*<0.001. (B) Triangular distribution. *Left:* Histogram of pulse magnitudes (peak fMRI signal), pooled across all participants. A linear distribution (black line) was fit to the data using a least-squares approach. *Right:* Adding simulated pulses, with magnitudes drawn from the linear distribution, increased FC between L-SM1_ue and L-dACC. Censoring simulated pulses partially reduced FC increases. *P*<0.05, **P*<0.01, ***P*<0.001.
Fig. S8. Functional Connectivity (FC) Changes Caused by Simulated Spontaneous Activity Pulses (All Participants). (A) Subtraction map showing changes in L-SM1, FC due to addition of simulated pulses. FC changes due to pulse addition closely matched FC changes during casting (Cast1: spatial correlation, $r = 0.44$, $P < 0.001$; Cast2: $r = 0.95$, $P < 0.001$; Cast3: $r = 0.64$, $P < 0.001$). (B) Subtraction map showing effect of censoring simulated pulses. Effects of censoring closely complemented the effect of pulse addition (Cast1: $r = -0.71$, $P < 0.001$; Cast2: $r = -0.96$, $P < 0.001$; Cast3: $r = -0.69$; $P < 0.001$).
Fig. S9. Functional Connectivity (FC) Decreases Were Not Explained by Spontaneous Activity Pulses. (A) Example regions of interest (ROIs) in the left and right primary somatomotor cortex (L-SM1ue and R-SM1ue). (B) Relationship of FC between L-SM1ue and R-SM1ue vs. the number of pulses detected. Each dot represents one 30-minute scan. Colored dots represent scans during the cast period. For all participants, FC between L-SM1ue and R-SM1ue was significantly correlated with the number of pulses detected (Cast1: \( r=0.74, P<0.001 \); Cast2: \( r=0.57, P<0.001 \); Cast3: \( r=0.73, P<0.001 \)). (C) Censoring pulses did not reduce the difference between Pre and Cast scans. ***P < 0.001. (D) Adding simulated pulses decreased FC between L-SM1ue and R-SM1ue in two participants (Cast2 and Cast3), but these decreases were much smaller than those observed during casting. ***P < 0.001. **P < 0.01.
REFERENCES

1. N. U. Dosenbach et al., Distinct brain networks for adaptive and stable task control in humans. Proc Natl Acad Sci U S A 104, 11073-11078 (2007).

2. T. N. Wiesel, D. H. Hubel, Comparison of the effects of unilateral and bilateral eye closure on cortical unit responses in kittens. J Neurophysiol 28, 1029-1040 (1965).

3. M. M. Merzenich et al., Topographic reorganization of somatosensory cortical areas 3b and 1 in adult monkeys following restricted deafferentation. Neuroscience 8, 33-55 (1983).

4. G. W. Milliken, E. J. Plautz, R. J. Nudo, Distal forelimb representations in primary motor cortex are redistributed after forelimb restriction: a longitudinal study in adult squirrel monkeys. J Neurophysiol 109, 1268-1282 (2013).

5. D. E. Feldman, M. Brecht, Map plasticity in somatosensory cortex. Science 310, 810-815 (2005).

6. D. S. Bassett, M. S. Gazzaniga, Understanding complexity in the human brain. Trends Cogn Sci 15, 200-209 (2011).

7. M. I. Posner, S. E. Petersen, The attention system of the human brain. Annu Rev Neurosci 13, 25-42 (1990).

8. M. E. Raichle et al., A default mode of brain function. Proc Natl Acad Sci U S A 98, 676-682 (2001).

9. G. L. Shulman, J. M. Ollinger, M. Linenweber, S. E. Petersen, M. Corbetta, Multiple neural correlates of detection in the human brain. Proc Natl Acad Sci U S A 98, 313-318 (2001).

10. B. Biswal, F. Z. Yetkin, V. M. Haughton, J. S. Hyde, Functional connectivity in the motor cortex of resting human brain using echo-planar MRI. Magn Reson Med 34, 537-541 (1995).

11. M. D. Fox et al., The human brain is intrinsically organized into dynamic, anticorrelated functional networks. Proc Natl Acad Sci U S A 102, 9673-9678 (2005).

12. M. D. Greicius, B. Krasnow, A. L. Reiss, V. Menon, Functional connectivity in the resting brain: a network analysis of the default mode hypothesis. Proc Natl Acad Sci U S A 100, 253-258 (2003).

13. B. T. Yeo et al., The organization of the human cerebral cortex estimated by intrinsic functional connectivity. J Neurophysiol 106, 1125-1165 (2011).

14. J. D. Power et al., Functional network organization of the human brain. Neuron 72, 665-678 (2011).

15. D. Cordes et al., Frequencies contributing to functional connectivity in the cerebral cortex in "resting-state" data. AJNR Am J Neuroradiol 22, 1326-1333 (2001).

16. M. J. Lowe, B. J. Mock, J. A. Sorenson, Functional connectivity in single and multislice echoplanar imaging using resting-state fluctuations. Neuroimage 7, 119-132 (1998).
17. M. D. Fox, M. Corbetta, A. Z. Snyder, J. L. Vincent, M. E. Raichle, Spontaneous neuronal activity distinguishes human dorsal and ventral attention systems. *Proc Natl Acad Sci U S A* **103**, 10046-10051 (2006).

18. W. W. Seeley *et al.*, Dissociable intrinsic connectivity networks for salience processing and executive control. *J Neurosci* **27**, 2349-2356 (2007).

19. N. U. Dosenbach, D. A. Fair, A. L. Cohen, B. L. Schlaggar, S. E. Petersen, A dual-networks architecture of top-down control. *Trends Cogn Sci* **12**, 99-105 (2008).

20. S. Marek, N. U. F. Dosenbach, Control networks of the frontal lobes. *Handb Clin Neurol* **163**, 333-347 (2019).

21. N. U. Dosenbach *et al.*, A core system for the implementation of task sets. *Neuron* **50**, 799-812 (2006).

22. E. M. Gordon *et al.*, Precision Functional Mapping of Individual Human Brains. *Neuron* **95**, 791-807 e797 (2017).

23. T. O. Laumann *et al.*, Functional System and Areal Organization of a Highly Sampled Individual Human Brain. *Neuron* **87**, 657-670 (2015).

24. D. Wang *et al.*, Parcellating cortical functional networks in individuals. *Nat Neurosci* **18**, 1853-1860 (2015).

25. S. Mueller *et al.*, Individual variability in functional connectivity architecture of the human brain. *Neuron* **77**, 586-595 (2013).

26. S. Marek *et al.*, Spatial and Temporal Organization of the Individual Human Cerebellum. *Neuron* **100**, 977-993 e977 (2018).

27. D. J. Greene *et al.*, Integrative and Network-Specific Connectivity of the Basal Ganglia and Thalamus Defined in Individuals. *Neuron* **105**, 742-758 e746 (2020).

28. R. M. Braga, R. L. Buckner, Parallel Interdigitated Distributed Networks within the Individual Estimated by Intrinsic Functional Connectivity. *Neuron* **95**, 457-471 e455 (2017).

29. R. A. Poldrack *et al.*, Long-term neural and physiological phenotyping of a single human. *Nat Commun* **6**, 8885 (2015).

30. C. M. Sylvester *et al.*, Individual-specific functional connectivity of the amygdala: A substrate for precision psychiatry. *Proc Natl Acad Sci U S A* **117**, 3808-3818 (2020).

31. D. J. Newbold *et al.*, Plasticity and Spontaneous Activity Pulses in Disused Human Brain Circuits. *Neuron* **107**, 580-589 e586 (2020).

32. J. D. Power, K. A. Barnes, A. Z. Snyder, B. L. Schlaggar, S. E. Petersen, Spurious but systematic correlations in functional connectivity MRI networks arise from subject motion. *Neuroimage* **59**, 2142-2154 (2012).

33. C. Gratton *et al.*, Emergent Functional Network Effects in Parkinson Disease. *Cereb Cortex* **29**, 2509-2523 (2019).
34. M. D. Greicius et al., Resting-state functional connectivity in major depression: abnormally increased contributions from subgenual cingulate cortex and thalamus. *Biol Psychiatry* **62**, 429-437 (2007).

35. A. Kucyi, J. Parvizi, Pupillary dynamics link spontaneous and task-evoked activations recorded directly from human insula. *J Neurosci* 10.1523/JNEUROSCI.0435-20.2020 (2020).

36. T. Harmelech, R. Malach, Neurocognitive biases and the patterns of spontaneous correlations in the human cortex. *Trends Cogn Sci* **17**, 606-615 (2013).

37. B. Guerra-Carrillo, A. P. Mackey, S. A. Bunge, Resting-state fMRI: a window into human brain plasticity. *Neuroscientist* **20**, 522-533 (2014).

38. C. M. Lewis, A. Baldassarre, G. Committeri, G. L. Romani, M. Corbetta, Learning sculpts the spontaneous activity of the resting human brain. *Proc Natl Acad Sci U S A* **106**, 17558-17563 (2009).

39. B. J. Shannon et al., Brain aerobic glycolysis and motor adaptation learning. *Proc Natl Acad Sci U S A* **113**, E3782-3791 (2016).

40. S. E. Petersen, M. I. Posner, The attention system of the human brain: 20 years after. *Annu Rev Neurosci* **35**, 73-89 (2012).

41. M. Neta, S. M. Nelson, S. E. Petersen, Dorsal Anterior Cingulate, Medial Superior Frontal Cortex, and Anterior Insula Show Performance Reporting-Related Late Task Control Signals. *Cereb Cortex* **27**, 2154-2165 (2017).

42. C. L. Wellman, L. L. Arnold, E. E. Garman, P. E. Garraghty, Acute reductions in GABAA receptor binding in layer IV of adult primate somatosensory cortex after peripheral nerve injury. *Brain Res* **954**, 68-72 (2002).

43. E. M. Gordon et al., Three Distinct Sets of Connector Hubs Integrate Human Brain Function. *Cell Rep* **24**, 1687-1695 e1684 (2018).

44. Z. P. Rosenthal et al., Local Perturbations of Cortical Excitability Propagate Differentially Through Large-Scale Functional Networks. *Cereb Cortex* **30**, 3352-3369 (2020).

45. M. Jacomy, T. Venturini, S. Heymann, M. Bastian, ForceAtlas2, a continuous graph layout algorithm for handy network visualization designed for the Gephi software. *PLoS One* **9**, e98679 (2014).

46. E. M. Gordon et al., Generation and Evaluation of a Cortical Area Parcellation from Resting-State Correlations. *Cereb Cortex* **26**, 288-303 (2016).

47. E. M. Gordon et al., Default-mode network streams for coupling to language and control systems. *Proc Natl Acad Sci U S A* **117**, 17308-17319 (2020).

48. B. Fischl, FreeSurfer. *Neuroimage* **62**, 774-781 (2012).

49. D. S. Marcus et al., Informatics and data mining tools and strategies for the human connectome project. *Front Neuroinform* **5**, 4 (2011).
50. J. Bottger, A. Schafer, G. Lohmann, A. Villringer, D. S. Margulies, Three-dimensional mean-shift edge bundling for the visualization of functional connectivity in the brain. *IEEE Trans Vis Comput Graph* **20**, 471-480 (2014).