Total lung capacity by plethysmography and high-resolution computed tomography in COPD

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Aim: To characterize and compare total lung capacity (TLC) measured by plethysmography with high-resolution computed tomography (HRCT), and to identify variables that predict the difference between the two modalities.

Methods: Fifty-nine consecutive patients referred for the evaluation of COPD were retrospectively reviewed. Patients underwent full pulmonary function testing and HRCT within 3 months. TLC was obtained by plethysmography as per American Thoracic Society/European Respiratory Society standards and by HRCT using custom software on 0.75 and 5 mm thick contiguous slices performed at full inspiration (TLC).

Results: TLC measured by plethysmography correlated with TLC measured by inspiratory HRCT (r = 0.92, P < 0.01). TLC measured by plethysmography was larger than that determined by inspiratory HRCT in most patients (mean of 6.46 ± 1.28 L and 5.34 ± 1.20 L respectively, P < 0.05). TLC measured by both plethysmography and HRCT correlated significantly with indices of airflow obstruction (forced expiratory volume in 1 second/forced vital capacity [FVC] and FVC%), static lung volumes (residual volume, percent predicted [RV%], total lung capacity, percent predicted [TLC%], functional residual capacity, percent predicted [FRC%], and inspiratory capacity, percent predicted), and percent emphysema. TLC by plethysmography and HRCT both demonstrated significant inverse correlations with diffusion impairment. The absolute difference between TLC measured by plethysmography and HRCT increased as RV%, TLC%, and FRC% increased. Gas trapping (RV% and FRC%) independently predicted the difference in TLC between plethysmography and HRCT.

Conclusion: In COPD, TLC by plethysmography can be up to 2 L greater than inspiratory HRCT. Gas trapping independently predicts patients for whom TLC by plethysmography differs significantly from HRCT.

Keywords: lung capacity, plethysmography, high-resolution computed tomography, gas trapping, lung volume measurement errors

Background
Estimation of lung volume is used to help categorize the type, severity, and progression of lung diseases, and their response to therapy. The overestimation of total lung capacity (TLC) by body plethysmography compared with high-resolution computed tomography (HRCT) (or, as some see it, the underestimation by HRCT compared with plethysmography) is well described in the literature. The degree to which TLC measured by body plethysmography differs from HRCT in COPD is not understood. This may have significant implications for determining patient eligibility for therapies such as lung volume reduction surgery, characterizing a prospective lung transplant recipient’s lung volume dimensions, or assessing the response to treatment. Our objective was...
to describe the degree to which TLC determination by body plethysmography differs from HRCT. Further, we sought to identify variables that may predict this difference.

Materials and methods

Study patients

A retrospective review was performed on 71 sequential patients referred to our outpatient clinic for the evaluation of COPD between September 2008 and December 2008. Patients who met the following criteria were extracted: (1) obstructive physiology evidenced by forced expiratory volume in 1 second (FEV$_1$)/forced vital capacity (FVC) $\leq$ 70 and TLC $\geq$ 80, (2) no or minimal radiographic abnormalities, or (3) complete pulmonary function tests (PFTs) and HRCT within 3 months.

PFTs

All patients underwent PFTs that were performed on a body plethysmograph (VMax Spectra 22D/62J; Carefusion, Yorba Linda, CA) according to the guidelines of the American Thoracic Society/European Respiratory Society. TLC was obtained as per American Thoracic Society/European Respiratory Society standards. Patients were excluded if they failed to meet criteria for reproducibility, which was defined as the patient demonstrating at least three functional residual capacity (FRC) values that agree within 5% (two patients), or if they failed to perform three to five technically satisfactory panting maneuvers at frequencies at or around 1 Hertz (two patients).

Chest HRCT

HRCT scans with 0.75 and 5 mm contiguous slices were performed at full inspiration using a 16 or 64 MDCT scanner (Somatom Sensation; Siemens Medical Systems, Erlangen, Germany). Technical parameters included kVp of 100–120 determined by estimation of body mass index. Patients underwent helical computed tomography (CT) of the entire lung at maximum inspiration in the supine position. Patients received breathing instructions by recorded voice commands from the CT scanner. Custom software (Pulmonary Workstation Plus, VIDA Diagnostics, Inc, Coralville, IA) was used to determine total lung volume, tissue volume, and air volume in milliliters, and mean lung density in Hounsfield units (HU) for each patient. All voxels marked as lung parenchyma were analyzed. Percent emphysema was determined as the percentage of voxels below thresholds of $-950$ and $-910$ HU. Total volume at full inspiration represents the TLC by HRCT for all analysis (Figure 1). HRCT scans were excluded from analysis for radiographic abnormalities other than emphysema including parenchymal consolidation, pleural effusion, and previous lung volume reduction surgery (LVRS) or transplant surgery (two patients). Patients were also excluded from analysis when the VIDA software was unable to process the scan.

Figure 1 Diagram of the lungs of a 61-year-old man with COPD. The transverse view (top left), coronal view (top right), and sagittal view (bottom left) are at the same anatomical level, as well as three-dimensional rendering of tracheobronchial tree (bottom right).
due to technical difficulties, including failure to identify the tracheobronchial tree (six patients).

Statistical analysis
Student’s t-test was used for comparison of TLC by plethysmography and HRCT. The Wilcoxon signed rank test was used where normality was not met. Spearman’s rank order correlation and Bland–Altman analysis were used for comparison of TLC by plethysmography and HRCT. Multiple linear regressions were used to determine which variables accounted for the ability to predict the difference between TLC measured by plethysmography and HRCT. Data are presented as mean ± standard deviation unless otherwise indicated.

Results
Demographics, pulmonary function data, and HRCT results obtained from the 59 patients are reported in Tables 1–3 respectively. Pulmonary function testing and HRCT were performed within 3 ± 20 days of each other. The subject population included 18 patients (31%) with Global Initiative for Chronic Obstructive Lung Disease (GOLD) II disease, 22 patients (37%) with GOLD III disease, and 19 patients (32%) with GOLD IV disease.8

Table 1 Demographics in 59 patients with COPD

| Variables          | Mean | SD or % total |
|--------------------|------|---------------|
| Age (years)        | 63   | 9             |
| Male               | 27   | 46%           |
| Caucasian          | 47   | 80%           |
| BMI                | 27   | 6             |
| Pack-years         | 41   | 18            |

Abbreviations: BMI, body mass index; pack-years, packs of tobacco smoked per day × years as a smoker; SD, standard deviation.

Table 2 Pulmonary function in 59 patients with COPD

| Variables           | Mean | SD |
|---------------------|------|----|
| FEV1/FVC            | 0.36 | 0.12 |
| FVC (L)             | 2.98 | 0.94 |
| FVC%                | 85   | 17  |
| FEV1 (L)            | 1.08 | 0.52 |
| FEV1%               | 41   | 18  |
| FEF 25–75 (L)       | 0.61 | 0.23 |
| FEF 25%–75%         | 29   | 20  |
| RV (L)              | 3.38 | 1.0  |
| RV%                 | 164  | 48   |
| TLC (L)             | 6.46 | 1.28 |
| TLC%                | 115  | 15   |
| RV/TLC              | 0.52 | 0.11 |
| FRC (L)             | 4.44 | 1.08 |
| FRC%                | 146  | 32   |
| IC (L)              | 2.02 | 0.73 |
| IC%                 | 86   | 22   |
| IC/TLC              | 0.31 | 0.09 |
| DLCO/VA             | 2.49 | 0.78 |
| DLCO/VA%            | 50   | 15   |

Abbreviations: DLCO/VA, carbon monoxide diffusing capacity corrected for alveolar volume; DLCO/VA%, carbon monoxide diffusing capacity corrected for alveolar volume, percent predicted; FEF 25–75 (L), forced expiratory volume during midexpiratory flow; FEF 25%–75%, forced expiratory volume during midexpiratory flow, percent predicted; FEV1, forced expiratory volume in 1 second; FEV1%, forced expiratory volume in 1 second, percent predicted; FVC, forced vital capacity; FVC%, forced vital capacity, percent predicted; IC, inspiratory capacity; RV, residual volume; RV%, residual volume, percent predicted; SD, standard deviation; TLC, total lung capacity; TLC%, total lung capacity, percent predicted.

As has been reported by others, there was fair correlation between TLC measured by both plethysmography and HRCT with indices of airflow obstruction (FEV1/FVC and FVC%), static lung volumes (residual volume, percent predicted [RV%], total lung capacity, percent predicted [TLC%], functional residual capacity, percent predicted [FRC%], inspiratory capacity, percent predicted), and percent emphysema. Both TLC by plethysmography and HRCT showed weak but significant inverse correlations with diffusion impairment (Table 5).

The difference between TLC as measured by plethysmography and HRCT correlated significantly with static

Table 3 HRCT in 59 patients with COPD

| Variables           | Mean | SD |
|---------------------|------|----|
| HRCT total volume (L)| 6.05 | 1.26 |
| HRCT tissue volume (L)| 0.71 | 0.16 |
| HRCT air volume (L)  | 5.34 | 1.20 |
| HRCT density (HU)    | –873.15 | 29.47 |
| Emphysema less than –950 (%) | 27.74 | 14.9 |
| Emphysema less than –910 (%) | 50.54 | 16.23 |

Abbreviations: Emphysema less than –950, percent of voxels with Hounsfield units less than –950; emphysema less than –910, percent of voxels with Hounsfield units less than –910; HRCT, high-resolution computed tomography; HU, Hounsfield units; SD, standard deviation.
lung volumes (RV%, TLC%, and FRC%) (Table 5, Figures 4 and 5). In patients with more severe air trapping and hyperinflation, the difference between TLC measured by plethysmography and that determined by HRCT increased. Using multiple linear regressions, RV% and FRC% independently predicted the differences between TLC measured by plethysmography and HRCT (Table 6).

Discussion

Thoracic gas volume (TGV) can be measured in several different ways. In patients with COPD, body plethysmography is usually preferred to nitrogen washout and gas dilution techniques because it is argued that the latter methods are unable to measure poorly ventilated or unventilated areas of the lung.14-16 While body plethysmography readily measures trapped air not in communication with the airways, it is not without its own inherent errors, particularly in patients with increased airway resistance. TGV is calculated using Boyle’s law which states that pressure and volume are inversely proportional when temperature is constant. Within the body box, pressure at the mouth may not reflect true pressure in the alveoli if airway resistance increases.17,18 If alveolar pressure is underestimated, thoracic gas volume will be overestimated. Rodenstein et al demonstrated this error in the measurement of lung volumes by plethysmography when airflow obstruction occurs, and found thoracic gas volume measured from pressure swings at the mouth (TGVm) to be 1 or more liters greater than thoracic gas volume measured from pressure swings in the esophagus (TGVes), an indirect measurement of pleural pressure.19 The authors went on to qualify this overestimation of TGV in the setting of airflow obstruction as being dependent on panting frequency.20 TGVm was 1 L greater than TGVes at panting frequencies of 2 Hz in asthmatics, while no difference was seen in those without asthma. At higher frequencies, the discrepancy further increased in asthmatics, again with no difference in those without asthma. At lower panting frequencies, no difference was found between the two groups.21 This relationship between panting frequency and the overestimation of lung volume by plethysmography has also been described in patients with COPD.22,23

HRCT is an important method for routine testing for COPD. With dedicated post-processing software, rapid and reproducible estimates of tissue and air volume, mean lung density, percent emphysema, and airway anatomy are now available.24,25 Standardized computer-generated HRCT instructions have improved reproducibility and accuracy.26,27

Table 4 Comparison of FEV1% with plethysmography and HRCT

| Variables                      | FEV1% | P     |
|--------------------------------|-------|-------|
| Plethysmography                | -0.25 | 0.06  |
| Plethysmography-HRCT           | 0.05  | 0.71  |
| HRCT total (L)                 | -0.22 | 0.10  |
| HRCT tissue (L)                | 0.26  | 0.05  |
| HRCT air (L)                   | -0.29 | 0.03  |
| HRCT density (HU)              | 0.48  | 0.00  |
| Emphysema less than −950 (%)   | -0.43 | 0.00  |
| Emphysema less than −910 (%)   | -0.49 | 0.00  |

Abbreviations: FEV1%, forced expiratory volume in 1 second; RV, residual volume; FRC, functional residual capacity; FVC, forced vital capacity; HRCT, high-resolution computed tomography; TLC, total lung capacity.
Lung volume measurement by HRCT remains fraught with predictable and unpredictable errors. Lung volume measurement by HRCT results in a reduction in the size of the various subdivisions of the lung. In normal subjects, vital capacity (VC) falls less than 10% when passing from the upright to the supine position, but a reduction of up to 25% has been described in patients with diaphragm dysfunction and respiratory muscle weakness, conditions commonly seen in patients with COPD. However, postural changes in VC in patients with COPD have not been well described. Unpredictable errors in the measurement of lung volumes by HRCT include difficulty with maximum inspiratory maneuvers and breath-holding techniques during scanning. Using spirometric gating, patients with severe airflow obstruction have not been shown to reproduce maximum inspiratory volumes during HRCT.

In similar patient populations, previous authors have shown strong correlations between TLC measured by plethysmography and HRCT (Zaporozhan et al, Coxson et al, and Gierada et al reported \( r = 0.90, 0.88, \) and 0.87, respectively). Given what we know about the limitations of plethysmography and HRCT in COPD, we expected to find a relationship between severity of airflow obstruction and the differences in the measurement of TLC between plethysmography and HRCT. If TLC by plethysmography is potentially overestimated in the setting of increased airway resistance, we postulated that as \( \text{FEV}_1 \) decreased there would be greater differences between TLC measured by plethysmography and HRCT. We further hypothesized that increased airways resistance and subsequent air trapping and hyperinflation would be associated with the overestimation of lung volumes by plethysmography. A recent paper by O’Donnell et al compared lung volumes by plethysmography and helium dilution with HRCT in COPD, with plethysmographic TLC found to be significantly greater than HRCT values, and plethysmographic overestimation of TLC reported to be greatest among subjects with \( \text{FEV}_1 < 30\% \) of predicted. This was not found to be the case in the current study as differences between TLC measured by plethysmography and HRCT.

### Table 5: Correlation coefficients for plethysmography, HRCT, and the difference between plethysmography and HRCT

| Variables                  | Plethysmography | HRCT | Plethysmography–HRCT |
|----------------------------|-----------------|------|-----------------------|
|                            | \( r \)         | \( P \) | \( r \)         | \( P \) | \( r \)         | \( P \) |
| FEV1/FVC                   | \(-0.39\)       | 0.00  | \(-0.35\)       | 0.01  | 0.02             | 0.88  |
| FVC (L)                    | 0.58            | 0.00  | 0.66             | 0.00  | 0.03             | 0.84  |
| FVC%                       | 0.06            | 0.65  | 0.02             | 0.87  | 0.11             | 0.40  |
| FEV1 (L)                   | 0.06            | 0.63  | 0.14             | 0.28  | 0.04             | 0.77  |
| FEV1%                      | \(-0.25\)       | 0.06  | \(-0.22\)       | 0.10  | 0.05             | 0.71  |
| FEF 25–75 (L)              | 0.09            | 0.57  | 0.08             | 0.69  | 0.07             | 0.80  |
| FEF 25%–75%                | \(-0.30\)       | 0.05  | \(-0.27\)       | 0.06  | 0.12             | 0.39  |
| RV (L)                     | 0.69            | 0.00  | 0.54             | 0.00  | 0.32             | 0.02  |
| RV%                        | 0.44            | 0.00  | 0.28             | 0.03  | 0.29             | 0.03  |
| TLC (L)                    |                |      | 0.90             | 0.00  | 0.31             | 0.02  |
| TLC%                       | 0.56            | 0.00  | 0.34             | 0.00  | 0.39             | 0.00  |
| RV/TLC                     | 0.07            | 0.60  | \(-0.06\)       | 0.67  | 0.16             | 0.21  |
| FRC (L)                    | 0.85            | 0.00  | 0.74             | 0.00  | 0.29             | 0.03  |
| FRC%                       | 0.48            | 0.00  | 0.33             | 0.01  | 0.27             | 0.04  |
| IC (L)                     | 0.38            | 0.00  | 0.43             | 0.00  | 0.04             | 0.78  |
| IC%                        | \(-0.02\)       | 0.87  | \(-0.06\)       | 0.67  | 0.07             | 0.60  |
| IC/TLC                     | \(-0.13\)       | 0.33  | \(-0.05\)       | 0.72  | \(-0.07\)       | 0.61  |
| DLCO/VA                    | \(-0.42\)       | 0.00  | \(-0.35\)       | 0.01  | \(-0.06\)       | 0.63  |
| DLCO/VA%                   | \(-0.42\)       | 0.00  | \(-0.35\)       | 0.01  | \(-0.05\)       | 0.71  |
| HRCT total (L)             | 0.90            | 0.00  |                |      | \(-0.06\)       | 0.64  |
| HRCT tissue (L)            | 0.39            | 0.00  | 0.52             | 0.00  | 0.10             | 0.43  |
| HRCT air (L)               | 0.92            | 0.00  | 0.98             | 0.00  | \(-0.08\)       | 0.56  |
| HRCT density (HU)          | \(-0.44\)       | 0.00  | \(-0.39\)       | 0.00  | 0.20             | 0.13  |
| % emphysema less than \(-950\) | 0.43            | 0.00  | 0.41             | 0.00  | \(-0.18\)       | 0.18  |
| % emphysema less than \(-910\) | 0.49            | 0.00  | 0.44             | 0.00  | \(-0.15\)       | 0.26  |

**Abbreviations:** DLCO/VA, carbon monoxide diffusing capacity corrected for alveolar volume; DLCO/VA%, carbon monoxide diffusing capacity corrected for alveolar volume, percent predicted; emphysema less than \(-950\), percent of voxels with Hounsfield units less than \(-950\); emphysema less than \(-910\), percent of voxels with Hounsfield units less than \(-910\); FEF 25–75 (L), forced expiratory volume during midexpiratory flow; FEF 25%–75%, forced expiratory volume during midexpiratory flow, percent predicted; FEV1, forced expiratory volume in 1 second; FEV1%, forced expiratory volume in 1 second, percent predicted; FRC, functional residual capacity; FVC, forced vital capacity; FVC%, forced vital capacity, percent predicted; HRCT, high-resolution computed tomography; HU, Hounsfield units; IC, inspiratory capacity; RV, residual volume; RV%, residual volume, percent predicted; TLC, total lung capacity; TLC%, total lung capacity, percent predicted.
plethysmography and HRCT did not change across GOLD stages. This relationship between airflow obstruction and the plethysmographic overestimation of TLC may not have been seen because the current study's population included a range of FEV₁ from normal to very severe, and may not be powered sufficiently for subgroup analysis among patients with very severe airflow obstruction. O'Donnell et al collected data from subjects at three hospitals where HRCT and plethysmographic technique may not have been standardized. Patients recruited from one of the hospitals undergoing evaluation for LVRS had substantially lower average FEV₁ than those from the other two hospitals. Subtle differences in HRCT and plethysmographic technique at this hospital may have driven the relationship between airflow obstruction and the overestimation of plethysmographic TLC.

Table 6 Multiple linear regressions

| Variables     | Plethysmography-HRCT |
|---------------|-----------------------|
| RV%           | -2.14                 | 0.04 |
| TLC%          | -0.88                 | 0.39 |
| RV/TLC        | 0.15                  | 0.88 |
| FRC%          | 2.33                  | 0.03 |

Abbreviations: FRC%, functional residual capacity, percent predicted; HRCT, high-resolution computed tomography; RV, residual volume; RV%, residual volume, percent predicted; TLC, total lung capacity; TLC%, total lung capacity, percent predicted.

Figure 4 Relationship between TLC% predicted and difference between lung volumes determined by plethysmography (pleth) and HRCT.

Notes: \( r = 0.39, P < 0.01 \).
Abbreviations: HRCT, high-resolution computed tomography; TLC%, total lung capacity, percent.

Figure 5 Relationship between RV% predicted and difference between lung volumes determined by plethysmography (pleth) and HRCT.

Notes: \( r = 0.29, P < 0.01 \).
Abbreviations: HRCT, high-resolution computed tomography; RV%, residual volume, percent.

Understanding the variability with which TLC by plethysmography differs from HRCT has important implications in the evaluation of patients with COPD. Global and regional measurements of lung volumes can be important in identifying patients who are most likely to benefit from LVRS. Similarly, precise volume determination is necessary to accurately identify suitable donor and recipient lungs for transplantation. Finally, the ability to precisely measure lung volume may be central to determining the importance of hyperinflation in COPD, and the impact of therapies geared to reducing end-expiratory lung volumes.

Conclusion

Total lung capacity measured by plethysmography is larger than that determined by HRCT in COPD. The degree to which TLC measured by plethysmography differs from that determined by HRCT is correlated with air trapping and hyperinflation. RV% and FRC% predict the difference between TLC determined by plethysmography and HRCT.
The method used to obtain TLC in severely hyperinflated patients needs to be considered when precise measurements are required for clinical decision making.

Acknowledgments and disclosure
This retrospective review was designed and executed by Dr Garfield. The manuscript was written by Dr Garfield and edited by Drs Marchetti and Criner. The authors have no disclosures or conflicts of interest to report with regard to the material put forth in this manuscript. This study was partially funded by the Pennsylvania Department of Health PA-DOH 02-70-02.

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