Application of Orthodontic Immediate Force on Dental Implants: Histomorphologic and Histomorphometric Assessment

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Aims: Application of force to implants is helpful, especially in orthodontic-implant therapies. The aim of this study was a histomorphologic and histomorphometric evaluation of peri-implant bone after immediate orthodontic and orthopedic forces comparing them with a control group. Materials and Methods: Eighteen dental titanium implants were inserted in the premolar region of three dogs. Implants were divided into three groups: (1) group with immediate orthodontic force of 300 NC, (2) group with immediate orthopedic force of 600 NC, and (3) control group. Implants were explanted with adequate amount of surrounding bone after 3 months and bone-implant contact (BIC), amount of lamellar bone (LB), amount of woven bone (WB), amount of inflammatory connective tissue, and the rate of the movement were investigated. ANOVA, t-test, paired t-test, and Pearson’s test were used to analyze the data using SPSS software version 16 at a significant level of 0.05. Results: Based on BIC, amount of lamellar and WB and the amount of inflammatory connective tissue, there was no significant difference between the three groups (300 centinewton (CN), 600–CN, and control group) (P > 0.05). In the 300-CN and 600-CN groups, the rate of movement was reported 0.41 and 0.94 with no significant differences (P = 0.38). Conclusion: 300-CN and 600-CN immediate static loads do not interfere with osseointegration phenomenon and it does not decrease the amount of BIC and LB. Implants can be moved by preserving osseointegration, and this movement is in direct relation with the amount of applied force.

Keywords: Bone-implant contact, dental implants, orthodontic immediate force, osseointegration

INTRODUCTION

Optimal implant location is an important therapeutic goal in implant dentistry which leads to an ideal occlusion and esthetic. Application of force to implants is helpful, especially in orthodontic-implant therapies. This treatment plan is growing among middle-aged patients, those who require tooth replacement and tooth location correction, and patients with anatomical limitations who receive misplaced implants and need to have their implants location corrected due to biomechanical and esthetic reasons. In some cases, due to biomechanical and anatomical limitations, the proper angulation of implants is compromised. To reach an appropriate prosthetic treatment outcome, angulation correction by applying orthodontic forces is required for misplaced implants.

Some studies state that immediate forces on implants lead to fibrous tissue formation around them, rather than direct bone contact, which is critical for a successful implant treatment. This theory arises from the idea that the necrotic bone, which surrounds newly placed implants, is not able to bear forces and to apply functional loads, new bone should be replaced; however, recent studies demonstrate that immediate force will not necessarily cause fibrous tissue formation, and it even stimulates the formation of a

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mature lamellar bone (LB) which is resistant to forces. 

Today, scientists believe that implants with an appropriate initial stability can receive immediate forces. In a study by Oyonarte et al., it was shown that implants, which were planted to provide an orthodontic anchorage, were moved due to applied forces exactly after primary osseointegration and the osseointegration condition did not change. Moreover, bone density and bone height were greater at the site of force application. Crismani et al. in his study on implants which were planted in palate, showed that 400-centinewton (CN) orthodontic force one week after implantation, led to 90% success rate, and increase in stability after 12 weeks. Now, the question is that will a direct contact between bone and implants occur if forces are applied before osseointegration? will this contact be the same at both tension and pressure sides? And can we move the implants with preservation of osseointegration? The present study was designed to histomorphologically and histomorphometrically assess the peri-implant bone following an application of immediate orthodontic and orthopedic forces and compare it with the control group.

**Materials and Methods**

**Preparation of dogs**

In this interventional and experimental study, three Iranian mixed-breed healthy dogs weighing around 25 kg and aged 2–3 years were involved.

First, to prevent probable cross infection of diseases, all dogs were vaccinated (the vaccines included: rabies, influenza, hepatitis, leptospirosis, and distemper), then 10 mg ketamine vials and 0.15 mg Rampon (Alfasan, Woerden, The Netherlands) were injected intramuscularly to prepare appropriate anesthesia. To continue anesthetic procedures, Isoflurane (Baxter, IL, USA) was used, and dextrose saline serum (Mahban Darou, Tehran, Iran) was used to balance electrolytes.

Lateral cephalometric radiographies were taken from maxilla and mandible of dogs. Impressions were taken from upper and lower jaws using polyvinyl siloxane (Asia Chemi Teb Co., Tabriz, Iran, under the license of Coltene-Switzerland) to make special trays. Dogs’ mouths were rinsed by chlorhexidine (Shahr Darou Laboratories, Tehran, Iran). According to the Helsinki declaration, first to fourth premolars were extracted. For each quadrant of the dogs’ mouth, 2 cartridges of lidocaine (Mahban Darou, Tehran, Iran) were attached to them as abutments, followed by measuring the speed was 800 rounds/min. For all of these procedures, physiological serum was used as a coolant agent.

Alignment pins (Ø2.2 mm, length 28 mm, titanium, Institut Straumann, Basel, Switzerland) and prepared surgical stents were used to make sure that the implants were placed parallel. The distance between two implants from the control group was at least 2 cm.

The burs were used according to manufacturer instruction, and the speed was 800 rounds/min. For all of these procedures, physiological serum was used as a coolant agent.

**Implants insertion**

Three months after, tooth extraction and proper bone healing, the dogs were anesthetized, following mentioned procedures. In addition, silicone impressions were taken from each quadrant to provide surgical stents for placing implants as parallel as possible to each other. To ensure appropriate healing of extraction sites, periapical and lateral cephalograms were taken. ITI implants (with 10 mm length and 4.1 mm diameter) with SLA surface (Institut Straumann AG, Basel, Switzerland) were provided.

After appropriate healing of the extraction site with intact bone formation, crestal incision was performed, and then periosteum was retracted by periosteal elevator. Bone was prepared in the implants site by 2.3 mm diameter round burs (round bur; stainless steel, Institut Straumann, Basel, Switzerland). Implants site preparation was done by following 4-step procedure:

1. Cortical bone was perforated by starter surgical bur with 1.4 mm diameter
2. 2.2 mm diameter pilot drill was used (pilot drill 1, short, Ø2.2 mm, length 33 mm, stainless steel, Institut Straumann, Basel, Switzerland)
3. 2.8 mm diameter pilot drill was used (pilot drill 2, short, Ø2.8 mm, Length 33 mm, stainless steel, Institut Straumann, Basel, Switzerland)
4. In the final step, twist drill with 3.5 mm diameter was used (twist drill 1, short, Ø3.5 mm, length 33 mm, stainless steel, Institut Straumann, Basel, Switzerland).

The burs were used according to manufacturer instruction, and the speed was 800 rounds/min. For all of these procedures, physiological serum was used as a coolant agent.

Insertion torque was recorded using a torque wrench (Drehmoment Ratsche, 20–60 Ncm, Dr Dental AG, Gommiswald, Switzerland) and implant stability quotient was calculated by means of Osstell (Integration Diagnostic, Savedalen, Sweden) in buccolingual and mesiodistal aspects. Before screwing the abutments, impressions of implants were taken by Open Tray Technique. To record the distance between implants (of both case and control groups), transfer copings were attached to them as abutments, followed by measuring the distance using a digital caliper (Mitutoyo, Kanagawa, Japan) with 0.01 mm accuracy. Each measurement was repeated twice, and the mean amount was considered. To make sure that the bone around each screw would not interfere with the bone around adjacent screw, 20 mm distance was considered between screws. After placing the three implants in each quadrant (in the site of extracted first to fourth premolars), periapical radiographs were prepared for the analysis of the bone and bone resorption. In addition, vertical height from shoulder of the implant to crest of bone was measured in mesial and distal aspects.

**Orthodontic force application**

To apply forces to implants, implants mounts were not removed. Immediately after placement of the implants, Ni-Ti coil springs (Sentalloy, GAC, Central Islip, NY, USA) were
attached to the middle part of 6 implants’ mounts by means of 0.012” ligature wires, in the way that the springs were stretched 20 mm (to have 300-CN force).

Six hundred centinewton force was applied to other 6 implants. Since appropriate Ni-Ti coil springs which apply 600-CN force were not found, 2 springs similar to those with 300-CN force were used simultaneously. It has been stated that applied force to the implant should be at minimum of 300-CN and maximum of 600-CN to make deformation of cortical and trabecular bone without significant necrosis.[13]

Last 6 implants were considered as control group, and they were not loaded.

Postoperative care

After the operation, dogs received an intramuscular ampule of Penicillin G Benzathine/Procaine Sodium 2:1:1 (Jaber-Pharma, Tehran, Iran) and a neutralized Sulfonamide (Pentrizole) (Jaber-Pharma, Tehran, Iran) 1cc/kg. To keep the dog’s oral health in an optimum condition, 0.12% chlorhexidine mouth rinse and brushing were used weekly. The dogs were fed with cooked ground chicken once a day from the day after the operation.

Changes follow-up

Six weeks after surgery, following anesthetizing the dogs, their mouths were rinsed using brush and chlorhexidine, springs were detached, and their force was rechecked. Furthermore, the stability of implants was assessed at this stage. Any loose implants were removed and replaced with a mini-implant on each side to continue the force application. After preparing and checking periapical radiographs, the springs were attached again. We have to mention that the springs were replaced only if deformation occurred. Twelve weeks after surgery, apical radiographs were provided in addition to final lateral cephalometric radiographs. Then, implants and springs were cleaned using chlorhexidine and brush, and the forces were checked followed by removing the springs. Afterward, the distances between implants were remeasured intraorally, by the same researchers, using the same unit. At this stage also, the measurements were repeated twice and the mean amount was considered.

Sterile techniques were considered during all procedures.

Extracting the specimens

Trephine burs with 10 mm diameter were used, to cut implants with adequate amount of bone out.

Histological preparation

Extracted specimens were kept in a glutaraldehyde solution for 6 h. Embedded in series of graded alcohol, they were dehydrated and mounted precisely in a self-cured transparent acrylic resin (Meliodent; Heraeus kulzer, Berkshire, UK). Ground sections were then prepared, using Microtome (Accutom-50, Stuers, Copenhagen, Denmark). Sections were made along implants’ frontal axis and in mesiodistal dimension with approximate 250–350 μm thickness. The specimens were then thinned to 100-150 μm using an abrasive. Following immersion of the specimens in glutaraldehyde (24 h), graded alcohol (50%, 60%, 70%, 80%, 90, and 100% concentrations; each for 2 h) and Eksikator including calcium and chlorine and covering the specimens with gold, the specimens were studied under electron microscope. Micrographs were provided with ×50, ×200 and ×1600 magnification (Zeiss, Jena, Germany) from mesial and distal (4 micrographs altogether).

Statistical analysis

ANOVA, t-test, paired t-test, and Pearson’s test were used to analyze the data using SPSS software version 16 (IBM corporation, NY, USA) at a significant level of 0.05.

Ethical considerations

Ethical approval was granted by the Torabinejad Dental Research Center with ID number of 287243. All procedures were conducted strictly in accordance with ethical standards and with the last update of the Helsinki declaration. The maintenance and care of the animals complied with the ethical guidelines of the Torabinejad Dental Research Center, Isfahan University of Medical Sciences, Isfahan, Iran. To preserve dogs’ chewing ability, their main posterior teeth (counted as molars) were not extracted. In this study, dogs were not euthanized after the procedures.

Results

One of the implants with 300-CN force and two of them with 600-CN forces were excluded from the study because of getting loose with no sign of inflammation or infection. In addition, one implant in control group was excluded because of bone damage during explanting the implant. Altogether, 5 implants with 300-CN, 4 implants with 600-CN, and 5 control implants remained. In this study, total bone-implant contact (BIC), total woven and LB, inflammatory and connective tissues were investigated separately at the tension and pressure sites [Figure 1].

Furthermore, to simplify the understanding of the evaluated criteria, abbreviations were used which are presented at Table 1.

Bone-implant contact

Mean total percentage of BIC (ToBIC) was 81.62% ± 13.62% for 600-CN group, 79.80 ± 9.25 for 300-CN group, and 71.98 ± 13.5 for control group [Table 2]. The mean ToBIC, BIC at tension side and pressure side were not significantly different among the studied groups (300-CN, 600-CN, and control) (P > 0.05).

Peri-implant lamellar bone

The mean percentage of total LB within 2 mm around implants was 62.40 ± 1.94 for control group, 62.10 ± 2.10 for 300-CN group, and 59.43 ± 2.63 for 600-CN group [Table 3]. Mean percentage of peri-implant LB at pressure side (PLB) for control group, 300-CN group, and 600-CN group was 62.40 ± 2.30, 62.60 ± 3.36 and 60.12 ± 2.17, respectively.
Mean percentage of peri-implant LB at tension side (TLB) was 62.40 ± 2.30, 61.60 ± 1.51 and 58.75 ± 3.20 for mentioned groups, respectively. The mean TLB and PLB did not show significant differences among groups (300-CN, 600-CN, and control) (P > 0.05).

**Peri-implant woven bone**

Mean percentage of total peri-implant woven bone within 2 mm around implant for control group, 300-CN group, and 600-CN group was 31.93 ± 0.68, 31.4 ± 3.13, and 33.31 ± 0.80, respectively [Table 4]. The mean TLB and PLB had not significant differences among groups (300-CN, 600-CN, and control) (P > 0.05).

**Connective and inflammatory tissue around implant**

Mean amount of connective and inflammatory tissues (CITs) within 2 mm around the implants were measured [Table 5]. No significant difference was observed among groups for each observed criteria (all P > 0.05).

**Implants movement**

Mean rate of orthodontic movement of implants was 0.41 ± 0.41 mm/12 week in 300-CN group and was 0.94 ± 0.90 mm/12 weeks in 600-CN was. Mann–Whitney test revealed no significant differences in the mean rate of implants movement between two groups (600-CN and 300-CN) (P = 0.38); however, the movement rate of 600-CN and 300-CN implants was significantly different in both groups from the control group (P < 0.05).

**DISCUSSION**

Recent studies have shown that immediate prosthetic forces which are applied on dental implants not only lower the risk of fibrous tissue formation but also stimulate the formation of mature LB which is resistant against destructive forces. On the other hand, it is also possible to apply forces to mini-implants. Therefore, if we apply orthodontic forces to dental implants and their surrounding bone behaves as there was only an immediate prosthetic loading without orthodontic forces, the quality of prosthetic treatments will significantly improve.

In the present study, a number of criteria, including BIC, lamellar and WB formation, fibrous tissue formation and...
Table 3: Statistical indexes for lamellar bone around implant (%) within 2 mm, total, at pressure side, and at tension side after 12 weeks

| Group   | Mean±SD | Minimum | Maximum | P    |
|---------|---------|---------|---------|------|
| ToLB    |         |         |         |      |
| 300-CN  | 62.10±2.10 | 59.50   | 64.50   | 0.143|
| 600-CN  | 59.43±2.63 | 55.50   | 61.00   |      |
| Control | 62.40±1.94 | 60.50   | 65.50   |      |
| PLB     |         |         |         |      |
| 300-CN  | 62.60±3.36 | 59.00   | 67.00   | 0.365|
| 600-CN  | 60.12±2.17 | 57.00   | 62.00   |      |
| Control | 62.40±2.30 | 60.00   | 65.00   |      |
| TLB     |         |         |         |      |
| 300-CN  | 61.60±1.51 | 60.00   | 63.00   | 0.100|
| 600-CN  | 58.75±3.20 | 54.00   | 61.00   |      |
| Control | 62.40±2.30 | 60.00   | 66.00   |      |

ToLB=Total percentage of observed lamellar bone; PLB=Lamellar bone at pressure side; TLB=Lamellar bone at tension side; SD=Standard deviation

Table 4: Statistical indexes for woven bone around implant (%) within 2 mm, total, at pressure side, and at tension side after 12 weeks

| Group   | Mean±SD | Minimum | Maximum | P    |
|---------|---------|---------|---------|------|
| ToWB    |         |         |         |      |
| 300-CN  | 31.40±3.13 | 26.00   | 33.50   | 0.373|
| 600-CN  | 33.31±0.80 | 32.50   | 34.00   |      |
| Control | 31.93±0.68 | 31.00   | 32.65   |      |
| PWB     |         |         |         |      |
| 300-CN  | 30.50±3.57 | 24.50   | 33.00   | 0.340|
| 600-CN  | 32.87±0.62 | 32.00   | 33.50   |      |
| Control | 31.86±1.32 | 30.00   | 33.00   |      |
| T WB    |         |         |         |      |
| 300-CN  | 32.30±2.72 | 27.50   | 34.00   | 0.423|
| 600-CN  | 33.75±2.06 | 32.00   | 36.00   |      |
| Control | 32.00±0.70 | 31.00   | 33.00   |      |

ToWB=Total percentage of observed woven bone; PWB=Woven bone at pressure side; T WB=Woven bone at tension side; SD=Standard deviation

Inflammation around implants and also their movements were investigated.

During the study, one of the implants with 300-CN and two of them with 600-CN forces were excluded from the study due to loss of integrity. There was no infection or inflammation around implants, thus the failure can be attributed to the occlusal functional overload, like one implant in Oyonarte’s et al. study on dogs which was excluded due to same reason. In this finding was consistent with former researches which were conducted on monkeys. In the present study, BIC was not significantly different among groups (P > 0.05) and mean values of BIC in the group with 600-CN force were higher than other groups. Oyonarte et al. also did not find any significant differences in BIC between control group and implants that had undergone 100 g force for 5 weeks followed by 300 g force for 17 weeks. Meslen et al. in their study, where they had placed 10 implants in 6 monkeys for 11 weeks and applied 100-CN, 200-CN, and 300-CN forces, found that mean BIC was 60.7% at the pressure side and 60.5% at tension side and 58.6% for the control group. No significant difference was observed among the groups. Satio et al. placed 18 Brenmark implants in 4 dogs, and 200 gr forces were applied for 24–32 weeks. In that study also, mean BIC was about 65%, and no difference existed among studied groups. Wehrbein et al. placed 10 implants in premolar area and palate of a dog, each with 10 mm length and 4 mm diameter. The implants underwent 200 gr forces for 26 weeks after an eight-week healing period. Microscopic investigations revealed that no difference was present between studied groups. In addition, it was proved that orthodontic force had even induced bone formation at pressure side. In the study by Rismanchian et al., 12 implants were placed in mandibles of three dogs, in the way that prosthetic nonfunctional force was applied for 6 implants, and the rest of them kept unloaded beneath the gingiva. In the mentioned study also, BIC was 51.33% and 44.4% for case and control groups, respectively; however, there was no significant difference between them.

Although BIC rates vary among different studies, they are in accordance with the present study, indicating not only there is no significant difference between control group and case groups but also there is no difference between tension and pressure sides. The difference between BIC is partly due to types of implants, duration of applied force, and also forces intensity since bone integrity is dependent on duration, frequency, type and distribution of force, and stress integrity. Moreover, in our study, orthodontic and orthopedic forces were applied immediately after implant placement, which can also imply for the different BIC rates compared to the previous studies. In a study by Degidi et al. where they investigated the bone remodeling after immediate loading, it was demonstrated that no difference exists between loaded and unloaded implants in terms of bone remodeling; however, higher amounts of LB were found around loaded implants.

On the other hand, it has been declared that immediate loading can increase the alveolar bone density around implant. Rismanchian et al., who placed 12 implants in mandibles of 3 dogs followed by immediate loading, demonstrated that no difference exists between osseointegration of loaded and unloaded implants and that formation of lamellar and WB is the same in both groups.

In the present study also, there was no difference between the groups in terms of formation of lamellar and WB which is consistent with the previous studies, but LB formation in control group was the highest and in 600-CN group was the lowest. This inconsistency with former researches could be attributed to the intensity and type of the force which was applied because mechanical stresses and strains are correlated to bone remodeling.

The first type of bone formed in orthodontic responses is WB. This may explain the higher percentage of WB formation in the 600-CN group compared to other groups.
In the present study, implants with 300- and 600-CN force moved 0.41 mm and 0.94 mm, respectively. In the study by Oyonarte et al., porous and machined implants which underwent 100 g force for 5 weeks and 300 g for 17 weeks moved 0.12 mm and 0.515 mm, respectively.[14] In Majzoub’s et al. study, one of the 20 implants which were placed in rabbit’s calvaria with 150 g-force moved 0.5 mm. These results show that the amount of implants’ movements depends on numerous criteria.[26]

In the present study, there was no significant difference among the three groups in terms of CIT formation; however, the mean amount of CIT in the 600-CN group was more than two other groups. It indicates that applying immediate orthodontic and orthopedic force after implant placement will not threaten implants’ success rate. To actualize the idea of applying immediate static forces to dental implants in humans, it is necessary to conduct more studies and investigate criteria such as diameter and length of implants, rate of resistant force, and different periods of force application. Moreover, it is recommended to investigate the bone response to force application by means of fluorescent markers and microradiographs which are capable of detecting bone remodeling after different periods.

### Conclusion

With limitations of this study, it can be concluded that immediate static loading with 300-CN and 600-CN might not interfere with the osseointegration procedure and might not decrease BIC and LB rates. The results of the study also demonstrated that it is possible to slightly move implants by applying static forces without tampering with osseointegration. However, more studies are suggested to provide more precise and determinant decision.

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### Conflicts of interest

There are no conflicts of interest.

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### Table 5: Statistical indexes for amount of connective and inflammatory tissues (% around implant within 2 mm, total, at pressure side and at tension side after 12 weeks

| Group | Mean±SD | Minimum | Maximum | P     |
|-------|---------|---------|---------|-------|
| ToCIT | 300-CN  | 6.50±1.90 | 4.50 | 9.50 | 0.465 |
|       | 600-CN  | 7.31±2.30 | 5.00 | 10.50 |       |
| Control | 5.67±1.57 | 3.50 | 7.00 |       |
| PCIT  | 300-CN  | 6.90±1.74 | 5.00 | 8.50 | 0.627 |
|       | 600-CN  | 7.12±2.65 | 5.00 | 11.00 |       |
| Control | 5.74±2.52 | 3.00 | 9.00 |       |
| TCIT  | 300-CN  | 6.10±2.65 | 4.00 | 10.50 | 0.519 |
|       | 600-CN  | 7.50±2.08 | 5.00 | 10.00 |       |
| Control | 5.60±2.50 | 2.00 | 9.00 |       |

TCIT=Connective and inflammatory tissues around the implant at tension side; PCIT=Connective and inflammatory tissues around the implant at pressure side; ToCIT=Total percentage of connective and inflammatory tissues; SD=Standard deviation.
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