The Contribution of Various MRI Parameters to Clinical and Cognitive Disability in Multiple Sclerosis

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Next to the disseminated clinical symptoms, cognitive dysfunctions are common features of multiple sclerosis (MS). Over the recent years several different MRI measures became available representing the various features of the pathology, but the contribution to various clinical and cognitive functions is not yet fully understood. In this multiparametric MRI study we set out to identify the set of parameters that best predict the clinical and cognitive disability in MS. High resolution T1 weighted structural and high angular resolution diffusion MRI images were measured in 53 patients with relapsing remitting MS and 53 healthy controls. Clinical disability was inflicted by EDSS and cognitive functions were evaluated with the BICAMS tests. The contribution of lesion load, partial brain, white matter, gray matter and subcortical volumes as well as the diffusion parameters in the area of the lesions and the normal appearing white matter were examined by model free, partial least square (PLS) approach. Significance of the predictors was tested with Variable Importance in the Projection (VIP) score and 1 was used for threshold of significance. The PLS analysis indicated that the axial diffusivity of the NAWM contributed the most to the clinical disability (VIP score: 1.979). For the visuo-spatial working memory the most critical contributor was the size of the bilateral hippocampi (VIP scores: 1.183 and 1.2 left and right respectively). For the verbal memory the best predictors were the size of the right hippocampus (VIP score: 1.972), lesion load (VIP score: 1.274) and the partial brain volume (VIP score: 1.119). In case of the information processing speed the most significant contribution was from the diffusion parameters (fractional anisotropy, mean and radial diffusivity, VIP scores: 1.615, 1.321 respectively) of the normal appearing white matter. Our results indicate that various MRI measurable factors of MS pathology contribute differently to clinical and cognitive disability. These results point out the importance of the volumetry of the subcortical structures and the diffusion measures of the white matter in understanding the disability progression.

Keywords: multiple sclerosis, BICAMS, atrophy, demyelination, cognition
INTRODUCTION

Multiple sclerosis (MS) is an inflammatory, demyelinating disease, which affects the central nervous system. Next to the disseminated clinical signs cognitive impairments are frequent symptoms, it can occur in 40–70% of the patients. Most commonly it affects the information processing speed, the episodic memory, the executive functions, and the visuospatial abilities. There are several psychometric surveys available, but the Brief International Cognitive Assessment for MS (BICAMS) allows a reliable, fast evaluation of the most frequently affected cognitive domains (1–3).

One of the most prominent feature of the disease is the white matter lesions identified on the MRI. The importance of these lesions is unquestionable and hence became cornerstone of the diagnosis (4) and the follow-up of therapeutic efficacy (5). However, the correlation of T2 lesion burden with clinical and cognitive impairment are modest at most, known as the clinico-radiological paradox (6, 7). Recently, increasing interest is shown about the gray matter (GM) atrophy, which has become an approach to follow-up of the therapeutic effectiveness (8, 9).

The fact that it correlates stronger with the clinico-cognitive functioning gives the real importance of the GM (10, 11). While lesions and gray matter atrophy are non-specific to the underlying pathology, there are novel methods which better approximate the pathological processes. One of those is diffusion tensor imaging, which non-invasively depicts the diffusion of water in biological tissues. The molecular diffusion is blocked by cellular elements (primarily membranes). This way the diffusion profile of the water depicts the microscopic components of the tissue architecture. It is important to notice, that the axon loss and the demyelination alters the diffusion profile differently. While the axon damage is demonstrated by the alterations in axial diffusivity, the changes of radial diffusivity allude to myelin damage. Diffusion tensor imaging, with appropriate parameters was able to detect widespread alterations of the white matter, even in the non-lesioned, normal appearing white matter (NAWM) (12). These alterations were also correlating with various clinical and cognitive functions (13, 14).

Several studies investigated the correlation between various MRI markers and clinical and cognitive dysfunction (14–17), but only a few study investigated the relative importance of these MRI parameters (18–20). Despite the undisputed merit these studies have limitations, as in some of the studies deployed only low number of diffusion directions, only some of the diffusion parameters were used, others did not include all of the subcortical structures separately in the analysis and cognitive domains were evaluated separately only by a few of the investigations.

Moreover, MRI parameters are highly related and that relationship is not trivial (12), conventional linear regression analysis could not unambiguously predict the importance of the variables. The model-free partial least square (PLS) approach, besides handling the problem of collinearity, is able to distinguish a pattern of those parameters that best predicts the variable in question. In the current investigation we set out to identify those MRI parameters, which could predict the clinical disability and various domains of cognitive dysfunction with the model free PLS approach.

MATERIALS AND METHODS

Subjects

The study was carried on 53 patients with relapsing-remitting MS diagnosis and 53 healthy, age-matched controls without history of any neurological or psychiatric diseases. Patients were enrolled from the Multiple Sclerosis Outpatient Clinic at the Department of Neurology. The diagnosis was founded on the 2005 revision of the McDonald criteria (21). The clinical disability was measured on the Kurtzke expanded disability status scale (EDSS) (22). The cognitive performance of patients was measured by Brief international assessment for MS (BICAMS). All patients were on disease-modifying therapy (Table 1). All of our patients were in a stable clinical condition, without relapses or EDSS progression in 6 months before or after the MR scans.

The study was approved by the National Institute of Pharmacy and Nutrition and the Regional Human Biomedical Research Ethics Committee (Ref. No.: 000002/2016/OTIG). All study participant gave their written informed contribution in accordance with the Declaration of Helsinki.

Cognitive Assessment of the Patients

The Brief International Cognitive Assessment for MS (BICAMS) test is a short form that is a fast, sensitive and specific tool for the determination of the cognitive disability of the patient. The BICAMS test involves 3 separate tests: the symbol digit modalities test (SDMT), the first five recall trials of the California verbal learning test II. (CVLT-II) and the first three recall trials of the brief visuospatial memory test revised (BVMT-R) (23).

In our study we used the validated Hungarian version of the BICAMS test [for details of the validation process see: (2)]. For all subtests of BICAMS the patient’s results were compared to the age matched control group of healthy from our earlier validation study (2) more than two standard deviation difference compared to the control database was considered as abnormal.

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### TABLE 1 | Demographic data of the subjects.

|                | Healthy | Patients |
|----------------|---------|----------|
| n              | 53      | 53       |
| Age (years; mean ± SD) | 36.06 ± 11.06 | 44.34 ± 11.51 |
| Sex (male)     | 16      | 17       |
| Education (year ± SD) | –       | 13.71 ± 2.4 |
| Disease duration (years; mean ± SD) | –     | 13.89 ± 9.02 |
| EDSS score     | –       | 1.89 ± 1.65 |
| Therapy        | –       | Interferon beta: 33 |
|                |         | glatiramer acetate: 20 |
| Duration of the therapy (years; mean ± SD) | – | Interferon beta: 3.89 ± 3.49 |
|                |         | glatiramer acetate: 4.0 ± 3.79 |
**Image Acquisition**
MR imaging were carried out on a 1.5T GE Signa Excite HDxt MR scanner. 3D spoiled gradient echo (FSPGR: TE: 4.1 ms, TR: 10.276 ms, matrix: 256 × 256, FOV: 25 × 25 cm, Flip angle: 15 degrees, in-plane resolution: 1 × 1 mm, slice thickness: 1 mm), FLAIR (TE: 133 ms, TR: 6000 ms, TI: 1848 ms, matrix: 256 × 256, FOV: 25 × 25 cm, Flip angle: 90 degrees, in-plane resolution: 1 × 1 mm, slice thickness: 1 mm) and 60 direction diffusion-weighted images with 6 non-diffusion-weighted reference volumes (TE: 93.8 ms, TR: 16,000 ms, matrix: 256 × 256, FOV: 23 × 23 cm, Flip angle: 90 degrees, in-plane resolution: 2.4 × 2.4 mm slice thickness: 2.4 mm, b: 1,000 s/mm²) were acquired for all subjects.

**Evaluation of Lesion Load**
Lesions were manually segmented on the FLAIR images by ET, and rechecked by ZTK having considerable experience in MS neuroradiology.

**Evaluation of Global Atrophy**
The partial brain volume (PBV) was calculated with SIENAX (24), part of FSL (25, 26). SIENAX started by extracting brain and skull images from the single whole-head input data (24). Tissue-type segmentation was then carried out (27) in order to calculate the partial volume of brain, the GM and WM.

**Volumetric Analysis of the Subcortical Structures**
Image analysis was carried out using tools of FSL (FMRIB Software Library, http://www.fmrib.ox.ac.uk/fsl) (25). To automatically segment the subcortical structures (28), FIRST, a deformable-model-based segmentation/registration tool was used that uses a Bayesian Appearance Model (FMRIB’s Integrated Registration Segmentation Toolkit). For the automatic segmentation of structures, shape and intensity variations of subcortical structures were constructed from a training set of 336 images. With preservation of the cross-subject vertex correspondence, surface meshes were obtained with a deformable model. At each vertex a sample was taken from the normalized intensities along the surface normal. Then the vertex location and intensity variation were modeled as a multivariate Gaussian distribution. Finally, maximizing the posterior probability of the shape given the observed intensities, this model was fit to new images (10, 29). The result of the segmentation was manually checked and corrected if necessary by the first author. The volume of the segmented subcortical structures were normalized to the head size.

**Microstructural Alterations of the White Matter**
Diffusion data were corrected for Eddy currents and movement artifacts by 12 degree-of-freedom affine linear registration to the first non-diffusion-weighted reference image. Diffusion images were processed by using FDT (FMRIB’s Diffusion Toolbox part of FSL: www.fmrib.ox.ac.uk/fsl/fdt/). Fractional anisotropy, mean diffusivity \([\lambda_1 + \lambda_2 + \lambda_3]/3\), axial diffusivity \(\lambda_1\) and radial diffusivity \([\lambda_2 + \lambda_3]/2\) to the principal diffusion direction were computed for the whole brain.

The Tract-Based Spatial Statistics (TBSS) method was used to reduce possible errors resulting from misalignment of the images: A non-linear registration tool (FNIRT), which uses a b-spline representation of the registration warp field, aligned all fractional anisotropy images to a 1 × 1 × 1 mm FMRIB58_FA standard space. The data on all patients were brought into the standard space, and the mean fractional anisotropy image was created and then fed into the fractional anisotropy skeletonization program, thresholded at fractional anisotropy = 0.2 to create a mean fractional anisotropy skeleton that represented the centers of all tracts common to the group. The aligned fractional anisotropy data on each subject were then projected onto this skeleton, which resulted in the 4D skeletonized fractional anisotropy image.

A voxel-wise alteration of the diffusion parameters, (microstructural integrity index—MII), was calculated for each patient (12), by comparing the value of every voxel with the distribution from the normal subjects in the spatially matching voxel (z-score). To identify a global white matter damage we calculate the averages of these z-scores:

\[
X_n = \frac{\sum_{i=1}^{q} X_{n,i}}{q},
\]

\[
\delta_n = \frac{\sum_{i=1}^{q} (X_{n,i} - X_{n,j})}{q},
\]

\[
Z_{X_n,i} = \frac{X_{n,i} - X_n}{\delta_{n}},
\]

where \(X\) is the measured diffusion parameter (fractional anisotropy, mean diffusivity, axial diffusivity, and radial diffusivity) in the \(n\)th voxel in the skeleton. Indices \(i\) and \(j\) are for controls and patients, respectively.

The average diffusion parameters were calculated for each patient in the lesions and normal appearing white matter: The lesions were projected to the fractional anisotropy skeleton. The manually segmented lesions were brought to the diffusion data space with 6 degree-of-freedom linear registration. Through use of the warp field and the skeleton projections of the TBSS analysis of the fractional anisotropy images, the lesion mask was brought to the skeleton with the FSL tbss_non_fa algorithm. The mask was finally thresholded at 0.5 and binarized to avoid any size increment arising from the interpolation.

**Analysis of the Connection Between the MR Parameters and the Clinical and Cognitive Status**
We used partial least square (PLS) regression analysis to estimate the contributions of the various MRI parameters (partial brain volume, normalized gray matter and white matter volume, volume of the subcortical structures, lesion load and the diffusion parameters of the lesions and the normal appearing white matter) to the EDSS and the subscores of the BICAMS test (Figure 1). If
Y is an \( n \times q \) matrix of dependent variables over \( n \) observations and \( X \) is an \( n \times p \) matrix of predictors. PLS successively extracts latent variables (factors and loadings) from \( X \) and \( Y \) in such a way that covariance between the factors and loadings is maximized. With this approach, PLS reduces the dimensionality of the data by providing a weighted linear combination of \( X \) variables to form orthogonal components that predicts the dependent variable. In mathematical terms, Partial least squares is a linear decomposition of \( X \) and \( Y \) such that

\[
X = TP^T + E, \\
Y = UQ^T + F
\]

and the covariance between \( T \) and \( U \) is maximum (30). In the above equations, \( T \) is the \( n \times r \) \( X \) scores, \( U \) is the \( n \times r \) \( Y \) scores, \( P \) is the \( p \times r \) \( X \) loadings, \( Q \) is the \( 1 \times r \) \( Y \) loadings, \( E \), and \( F \) are residuals, and \( r \) is the number of extracted latent variables. The statistical inference on the significance of the latent variable was carried out by permutation tests on the singular values of the decomposition. The elements of the dependent variable matrix were randomly permuted 5,000 times and the singular value was recalculated to depict a null distribution. The summary of the importance for the \( X \) loadings was calculated by a Variable Importance in the Projection (VIP) score (31). Since the average of squared Variable Importance in the Projection scores is equal to 1, the “greater than one” rule was used for the selection of the important variables.

**RESULTS**

**Clinical, Cognitive, and Imaging Parameters of the Patients**

The patients recruited in our study have mild to moderate disability as measured by EDSS in spite of the relatively long disease duration (Table 1). Out of the 53 patients 18 had cognitive dysfunction on one cognitive test (CVLT: 0, BVMT: 7, SDMT: 9), 8 on two tests (SDMT and BVMT: 7, BVMT and CVLT: 1) and 5 on all three tests.
### TABLE 2 | MRI parameters and cognitive scores of the subjects.

| Subcortical Structure volume mm³ (mean ± SD) | Multiple sclerosis | Healthy | p-value |
|---------------------------------------------|-------------------|---------|---------|
| Left amygdala                               | 1717.22 ± 304.80  | 1755.28 ± 235.315 | 0.473   |
| Left caudatus                               | 4234.02 ± 611.32  | 4683.56 ± 561.583 | 0.02    |
| Left hippocampus                            | 5019.21 ± 608.16  | 5434.64 ± 690.22  | 0.001   |
| Left pallidum                               | 2303.76 ± 328.13  | 2383.04 ± 187.67  | 0.130   |
| Left putamen                                | 6270.55 ± 749.85  | 6802.61 ± 601.27  | 0.000106|
| Left thalamus                               | 965.38 ± 1092.743 | 10886.14 ± 837.47 | 0.00000 |
| Right amygdala                              | 1666.32 ± 264.20  | 1713.80 ± 311.28  | 0.399   |
| Right caudatus                              | 4414.96 ± 705.49  | 4905.77 ± 582.28  | 0.000167|
| Right hippocampus                           | 5148.92 ± 551.24  | 5340.47 ± 663.50  | 0.109   |
| Right pallidum                              | 2331.54 ± 250.36  | 2435.00 ± 181.80  | 0.017   |
| Right putamen                               | 6248.99 ± 765.47  | 6658.91 ± 628.22  | 0.003   |
| Right thalamus                              | 9380.61 ± 1092.52 | 10521.75 ± 925.85 | 0.00000 |

| Global atrophy (mean ± SD)                  | Normalized PBV    | Normalized GM volume | Normalized WM volume |
|---------------------------------------------|-------------------|----------------------|----------------------|
|                                             | 1423745.72 ± 7726.26 | 1492340.43 ± 65602.53 | 0.332               |
|                                             | Normalized GM volume | 784317.27 ± 51061.79 | 824838.22 ± 44204.64 | 0.00003            |
|                                             | Normalized WM volume | 639428.45 ± 43973.57 | 667502.21 ± 36040.49 | 0.000498           |

| Diffusion parameters % (mean ± SD)          | NAWM_FA           | Lesioned_FA          | NAWM_AD              | Lesioned_AD         |
|---------------------------------------------|-------------------|----------------------|----------------------|---------------------|
|                                             | 94.46 ± 5.78      | 89.90 ± 14.36        | 100.85 ± 2.41        | 105.66 ± 10.07      |
|                                             |                   | NAWM_MD              | 103.84 ± 5.14        | 112.83 ± 18.62      |
|                                             |                   | Lesioned_MD          | 108.06 ± 9.83        | 123.63 ± 35.29      |

| Lesions LL (mean ± SD)                      | 9698.33 ± 9754.94 | –                    | –                    | –                   |

| Cognitive scores (mean ± SD)               | BVMT z-score      | SDMT z-score         | CVLT z-score         |
|--------------------------------------------|-------------------|----------------------|----------------------|
|                                            | −0.67 ± 1.49      | −1.00 ± 1.22         | 0.28 ± 0.98          |

For the measured MRI parameters (partial brain volume, GM and WM volume, volume of the subcortical structures and the diffusion parameters of the white matter) see Table 2.

**The Imaging Parameters Influencing Clinical Disability**

In the first PLS analysis, the dependent variable was the EDSS. As the second latent variable interpreted only a small part of the variance of the dependent measure (<10%) and the permutation test indicated a non-significant latent variable, only the first latent variable was evaluated. The permutation test showed that the first latent variable was significant (p < 0.001) and responsible for 50.67% of the variation of the dependent variable and 27.08% of the predictors. The X loadings and the corresponding VIP scores indicated that age (VIP score: 1.72) and the axial diffusivity of the NAWM contributed the most to the clinical disability (VIP score: 1.979) (Figure 2). While far less, but still significant contributor was from the mean diffusivity of the NAWM (VIP score: 1.169), the demyelination features of the lesions (VIPFA: 1.17, VIPRD: 1.08).

**The Imaging Parameters Influencing Cognitive Functions**

In these analyses the raw scores from the three subtest of the BICAMS test were used as dependent variables. The first latent variable was evaluated, as the second latent variable was responsible for just a small fraction of the variance of the dependent measure (<5% in case of BVMT and CVLT and 10% in case of SDMT) and the permutation tests indicated non-significant latent variables. The permutation test indicated that the first latent variable was significant (p < 0.001 for each subtests) and explained for 50.99% of the variation of the dependent variable and 23.89% of the predictors in case of the BVMT, for 50.93% of the variation of the dependent variable and 22.24% of the predictors in case of the CVLT, for 50.67% of the variation of the dependent variable and 22.43% of the predictors in case of the SDMT.
Age contributed significantly to all cognitive tests (VIP score: 1.538, 1.127, and 1.296 for BVMT, CVLT, and SDMT, respectively). Gender was significant contributor to CVLT and SDMT (VIP score: 1.356 and 1.345, respectively).

As regarding the *visuo-spatial working memory*, the most critical contributor was the size of the bilateral hippocampi (VIP scores: 1.183 and 1.2 left and right, respectively) and the demyelination features of the lesions (VIP<sub>FA</sub> score: 1.257, VIP<sub>MD</sub> score: 1.008, VIP<sub>RD</sub> score: 1.158) and the axon loss diffusion features of NAWM (VIP<sub>FA</sub> score: 1.125, VIP<sub>L1</sub> score: 1.232) (*Figure 3*). Lesion load was also a marginally significant contributor (VIP score: 1.031).

For the *verbal memory* the best predictor was the size of the right hippocampus (VIP score: 1.972), the lesion load (VIP score: 1.274), the partial brain volume (VIP score: 1.119) the total white matter volume (VIP score: 1.008), total gray matter volume (VIP score: 1.058), the size of the right caudate (VIP score: 1.152), and the FA of the NAWM (VIP score: 1.012) (*Figure 3*).

In case of the *SDMT test* the most significant contribution was from the demyelination-like diffusion parameters of the NAWM (fractional anisotropy and radial diffusivity VIP scores: 1.615, 321, respectively) (*Figure 3*). The FA, mean and the radial diffusivity of the lesions (VIP scores: 1.289, 1.082, and 1.271, respectively) and the size of the right hippocampus (VIP score: 1.101) also contributed significantly to the performance.

**DISCUSSION**

Our model-free analysis of multiparametric MRI data of MS patients revealed complex interplay between the clinical and cognitive disability and various MRI parameters. Clinical disability was best predicted by the axial diffusivity of the NAWM. Cognitive functions were influenced by several factors in the various domains: (i) the most critical MR contributor to the visuo-spatial working memory was the size of the bilateral hippocampi and the demyelination-like diffusion profile of the lesions, and the axon loss of the NAWM; (ii) the best predictor of the verbal memory was the size of the right hippocampus and the brain, gray and white matter volumes, and (iii) information processing speed as measured on the SDMT test was best predicted by the demyelination like diffusion parameter alterations of the white matter.

It is long known that correlation between clinical disability and lesion load is weak (6, 7). The correlation of disability with brain atrophy and primarily gray matter atrophy seems to be stronger (10, 32–36), however several voxel-wise morphometry studies failed to find correlation of focal gray matter atrophy and disability (37–42). There are conflicting results on the correlation between diffusion metrics and disability. Griff in a ROI analysis found neither abnormal diffusion parameters in the NAWM nor correlation with disability (43). Filippi et al. (44) found modest correlation between disability and the mean diffusivity of lesions. Hasan found no connection between the fractional anisotropy of the corpus callosum and the disability of patients (45). The anisotropy of the pyramidal tract was correlating with the EDSS in 25 relapsing-remitting MS patients (46). In a whole brain TBSS analysis Onu et al. found widespread differences between controls and MS patients and within these group differences FA correlated with EDSS, hand function and ambulation (47). Ciccarelli and colleagues found connection of the clinical disability with the FA of the supra and infratentorial NAWM. In particularly the FA and MD of the cerebral peduncles showed a negative correlation with the clinical disability, measured by EDSS (48). Importantly, most of the above mentioned studies limited the analysis to FA. Also the extent of microstructural damage reported was usually far less. Previous studies have demonstrated that the radial and axial diffusivity alterations indicate demyelination and axonal pathology, respectively (49–53). In our previous analysis we showed that the demyelination like diffusion parameter changes can be detected in most of investigated white matter skeleton if high number of diffusion directions are investigated (12). Interestingly, our current analysis pointed out, that the clinical disability was best defined by the axial diffusivity of the NAWM.

In recent years cognitive dysfunction in MS become the focus point of research. Patients with multiple sclerosis are usually more concerned about their cognitive impairments, than physical disability, and it has a greater influence on their quality of life (54). Earlier results even suggest that there is an accelerated disease progression in the cognitively impaired patients (55).
Therefore, the research of the structural background of the cognitive dysfunction cannot be overrated. Recently, BICAMS test, a reliable fast tool for cognitive survey become available, but the structural brain abnormality measured with this test was not systematically investigated.

Not only lesion burden, but lesion localization is a weak predictor of cognitive functions (7). There are several studies showing connection between gray matter atrophy and cognitive functions of MS patients. The volume of the thalamus was found to be associated with information processing speed (56), the attention/executive function and also the verbal memory (57). The volume of the putamen correlated with the information processing speed (SDMT test) (11). Hippocampal atrophy also showed a connection to cognitive dysfunction (58–60). In a multicenter study the atrophy of the hippocampus and the deep GM nuclei was found to be the best predictor of cognitive decline.
in MS, while the atrophy developed in the WM was associated with the disability of the patients (61).

The thinning of the different regions of the cortex shows connection with various cognitive functions. While the verbal memory performance showed connection with the cortical thinning in the insula, the visual memory performance correlated to parietal atrophy (62), the reduced verbal fluency was associated to the left-sided, while the impaired figural fluency was related to the right-sided cortical thinning in the anterior cingulate region (63). The auditory information processing speed measured with PASAT shows correlation with the thinning of the orbito-frontal cortex (64).

While the above mentioned studies provide evidence about the relationship of cognitive test and certain MRI measures, only limited number of studies investigated the relative contribution of various structural MRI parameters to clinically relevant set of cognitive test. Our results indicate that the three subtest of the BICAMS is related to the pathology of different brain structures.

The most critical contributor to the visuo-spatial working memory was the size of the bilateral hippocampi. An earlier study investigating the correlation between various cognitive functions and the components of the thalamic-hippocampal-prefrontal network found no correlation with the visuo-spatial abilities of the patients and the volume of the hippocampus, but the best predictor of the 7/24 Spatial-Recall Task was the uncinate fasciculus connecting the mediotemporal structures to frontal cortex (57). Other studies found the performance of MS patients on visuospatial memory tests correlated with the diffusion parameters of the fornix, the primary hippocampal efferent (65, 66), but not the volume of the hippocampus itself (65). Importantly, the structural abnormality of one structure usually comes along with the other structures connected functionally or structurally (67).

Performance of the verbal memory test was best predicted by the volume of the total gray matter and right hippocampus. Interestingly in the above mentioned study of Dineen on a smaller MS group the volume of the hippocampus did not show correlation with the verbal or the visuo-spatial memory scores (65). Kiy and colleagues found association between the consolidation score of the CVLT test and the right temporal horn volume, an indirect measure of hippocampal atrophy (68). A recent study found correlation between physical activity induced hippocampal viscoelasticity and improvement on CVLT-II test in MS patients (69). Global brain atrophy was found to be correlated with the CVLT long delay recall (52). The learning score of the CVLT-II was correlating with the size of the hippocampus, thalamus, caudate and amygdala, but not with the lesion burden or the brain parenchymal fraction in Benedict's study. According to the linear regression analysis the volume of the caudate predicts the verbal learning ability best (70).

The laterality of the hippocampal atrophy correlating with cognitive performance is also interesting. While in case of the BVMT the both hippocampi were similarly predictors of the cognitive function, in case of the CVLT the right hippocampus was significant predictor but not the left. This later is especially interesting since earlier studies showed that left hippocampal volume was related to verbal while the right to the visuospatial memory (71–73).

Recent study of Yu found extensive demyelination-like diffusion alterations in the white matter of MS patients spreading well into the NAWM (74). Most of these microstructural alterations correlated with the performance on the SDMT. Importantly out of the three cognitive test SDMT had the largest area of correlation. Another investigation found SDMT performance be correlated with the gray matter fraction and a diffusion measure of the brain parenchyma (18). Interestingly, the authors used a summary statistics for the diffusion metrics similar to our analysis.

Finally, it is important to consider the methods used in the current analysis. There are two important features of our analysis that needs to be considered. (i) We created a clinically feasible, new whole brain summary measure of the diffusion properties, respecting voxel-wise normal variation of the white matter microstructure. This approach is useful, when a large extent of the diffusion parameters are altered, such as in multiple sclerosis (12).

(ii) The contribution of pattern of diffusion parameters to the clinical and cognitive disability was examined by model-free partial least square analysis. If the predictors show high degree of collinearity (like MRI data), the conventional regression analysis might be misleading.

Partial least squares, besides handling the problem of collinearity, is able to distinguish a pattern of those parameters that best predicts the variable in question.

LIMITATIONS

The main strength of our study is that we have identified the independent contribution of various MRI parameters to the cognitive and clinical disability in MS. Nevertheless, it has to be emphasized that several other quantitative MRI markers were described in multiple sclerosis, such as magnetization transfer imaging, myelin water fraction etc. Including more predictors could possibly give a more thorough characterization of the dysfunction. Moreover, an important weakness of the approach used in our analysis that we were not considering the spatial distribution of the cortical atrophy. Alternative approaches, such as linked independent component analysis (67) could offer a better characterization of the focal alteration of MRI parameters. It also have to be mentioned that the clinical applicability of these approach is somewhat limited because of the lengthy data acquisition and processing approaches. However, with advancing MR technology, by establishing the minimum requirements of acquisition parameters (e.g., number of diffusion directions) and improvement of analysis approaches advanced quantitative measures should be available for the clinical practice too.

CONCLUSIONS

In MS there is a complex pathology of focal lesions and diffuse neuro-glial degeneration affecting the gray matter (cortical and
subcortical) and also the white matter. These various MRI measurable factors contribute differently to clinical and cognitive disability. Our results indicate that the volumetry of the cortical and subcortical structures and the diffusion measures of the white matter are critical for understanding the disability progression and these measures should be considered in clinical trials and in the everyday clinical practice.

DATA AVAILABILITY STATEMENT
All datasets for this study are included in the manuscript and the Supplementary Files.

AUTHOR CONTRIBUTIONS
ET, NS, and ZK contributed conception and design of the study. PF, AK, and DS organized the database. BK, KK, and DV performed the statistical analysis. ET wrote the first draft of the manuscript. KB and LV wrote sections of the manuscript. All authors contributed to manuscript revision, read, and approved the submitted version.

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SUPPLEMENTARY MATERIAL
The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fneur.2018.01172/full#supplementary-material

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