The J-PET detector - a tool for precision studies of ortho-positronium decays

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Abstract

The J-PET tomograph is constructed from plastic scintillator strips arranged axially in concentric cylindrical layers. It enables investigations of positronium decays by measurement of the time, position, polarization and energy deposited by photons in the scintillators, in contrast to studies conducted so far with crystal and semiconductor based detection systems where the key selection of events is based on the measurement of the photons’ energies. In this article we show that the J-PET tomograph system is capable of exclusive measurements of the decays of ortho-positronium atoms. We present the first positronium production results, its lifetime distribution measurements and discuss estimation of the influence of various background sources. The tomograph’s performance demonstrated here makes it suitable for precision studies of positronium decays including entanglement of the final state photons, positron annihilation lifetime spectroscopy plus molecular imaging diagnostics.

Keywords: Positron Emission Tomograph, Plastic scintillators, Positronium

1. Introduction

The J-PET detector, Jagiellonian Positron Emission Tomograph, developed in Cracow \cite{1,2} is a new tool for precision studies of positronium decays. The J-PET programme focuses on fundamental studies...
of positronium decays \cite{3-10}, on positron annihilation lifetime spectroscopy (PALS) \cite{11} as well as medical
diagnostics \cite{12-16}. The J-PET detector is a new PET device based on plastic scintillators designed for
total body scanning in medicine as well as for biological applications \cite{11, 17-19} and fundamental physics
research \cite{20} with detection of positronium via Compton rescattered photons in the detector.

In this paper we present the first ortho-positronium, o-Ps, production results from J-PET as well as
lifetime distributions that can be compared with theoretical predictions coming from previous simula-
tions \cite{21, 22}. These results, especially the identification of o-Ps decays, are the first obtained using a detector
based solely on plastic scintillators. Previous studies of o-Ps decays were conducted with crystal and semi-
conductor based detection systems. In addition, by using specific and realistic detector simulations we are
able to estimate the extent to which we can reduce the background influence on the distributions.

Positronium, an “atom” consisting of an electron and a positron, is described by bound state QED
with very small radiative corrections from Quantum Chromodynamics and weak interaction effects in the
Standard Model. Positronium comes in two ground states, $^1S_0$ para-positronium, denoted p-Ps, with spin
equal to zero and $^3S_1$ ortho-positronium, denoted o-Ps, with spin equal to one. p-Ps is slightly lighter
by 0.84 meV due to the interaction between the electron and positron spins and also the existence of the
o-Ps one-photon virtual annihilation processes. Spin-zero p-Ps has a mean lifetime of 125 picoseconds and
spin-one o-Ps has a mean lifetime of 142 nanoseconds in vacuum.

Reviews of positronium physics are given in \cite{23, 24}. Measurements of positronium decay rates are so
far consistent with bound state QED theoretical predictions performed in the framework of non-relativistic
QED \cite{25}. However, the present experimental uncertainties $\sim \mathcal{O}(10^{-4})$ are much larger than the theoretical
uncertainties (assuming the non-relativistic QED approach) by a factor of 100 for o-Ps and by 10,000 for
p-Ps, thus calling for increased experimental precision. Additional observables \cite{20} in positronium decays
involving correlations between the positronium’s spin and the momenta and polarization of the photons
emitted in the decays can be used to test discrete symmetries $C$, $CP$ and $CPT$ in o-Ps bound state decays.
Information about the photons’ polarization is deduced from the observation of the Compton scatterings
between pair of scintillators in the detector \cite{22, 26}. Charge conjugation invariance in this system has been
tested up to the level of $10^{-6}$ \cite{3-5} and the symmetries $CP$ \cite{6, 7} and $CPT$ \cite{8, 9} have so far been tested
up to $\mathcal{O}(10^{-3})$.

Possible invisible decays of positronium are also an interesting topic of investigation with the J-PET
detector \cite{27}. Mirror matter models of dark matter allow a branching ratio for the invisible decay of o-Ps
in vacuum to mirror particles up to about $2 \times 10^{-7}$, below the present experimental bound of $3.0 \times 10^{-5}$
With J-PET, the experimental accuracy on the total decay rate and discrete symmetries observables is expected to be improvable by an order of magnitude in precision. Studies of positronium decays have important applications also in medicine and biology. Inside biological materials the positronium mean lifetime and formation probability depend significantly on the healthiness of the tissue material, its nanostructure and concentration of bioactive molecules, in effect allowing us to distinguish between healthy and altered tissue. These factors are indicative of the stage of development of metabolic disorders of human tissues. Thus, positronium decay studies can provide new input in medical diagnosis. Other important applications are to chemistry and material characterization.

The plan of the paper is as follows. In Section 2 we describe the J-PET detector setup. Section 3 discusses the event selection method and results. Conclusions are given in Section 4.

2. J-PET detector and positronium production method

The J-PET detector (Fig. 1-left) is built from polyvinyl toluene base EJ-230 plastic scintillator strips with dimensions \(50 \times 1.9 \times 0.7 \text{ cm}^3\), arranged in three concentric cylindrical layers with radius 42.5 cm, 46.75 cm and 57.5 cm (Fig. 1-right). Each scintillator is connected from both sides with vacuum photomultipliers R9800. It allows one to reconstruct the position along the scintillator based on the time difference between signals registered at photomultipliers connected to the same scintillator. The scanner is equipped with the dedicated solely digital field programmable gate array platform (FPGA) and triggerless data acquisition system based on TRB3 hardware, optimised for detection of photons originating from positronium decay and photons from the nuclear deexcitations in the energy region of 1 MeV. Signals from the photomultipliers are transferred to the acquisition system and scanned at four different thresholds - 80 mV, 160 mV, 240 mV and 320 mV. Next, the data in the form of list-mode is further transferred to the analysis software. Analysis is performed with a dedicated analysis and simulation framework. Photons below 10 MeV energy interact in the plastic scintillators predominantly via the Compton effect. Therefore, the information about the energy of the photons is not available directly, and the whole data selection and analysis chain is based on the determination of the time and position of the photon’s interaction and its energy deposition. The time and position resolutions achieved with the J-PET detector are about 380 ps and 4.6 cm (in FWHM), respectively. This corresponds to the angular resolution equal to about 2.4 degree (in FWHM). Comparing to other large area detectors like Gammasphere or APEX array, the J-PET detector is characterized by better time resolution (4.6 ns for Gammasphere, 2 ns for APEX array.
In addition, due to trigger-less data acquisition system, the J-PET detector is capable of overcome the limitation of pileup events coming from higher rates of the positronium production, which allows to use higher source activities (10 MBq for the J-PET compared to 0.37 MBq for Gammasphere and APEX array). It provides the possibility to obtain higher statistic, which allows to obtain much more accurate results in the fundamental physics studies.

Figure 1: (left) Photograph of the J-PET detector with the annihilation chamber placed in the centre of the detector with a pipe installed on the detector axis. (right) Schematic cross section of the J-PET detector. Black rectangles indicate the cross section of scintillator strips arranged in three concentric cylindrical layers. The arrows indicate annihilation photons (red) from ortho-positronium and the de-excitation photon (blue) emitted by the $^{22}\text{Na}$ source located at the centre of the detector.

Following part is the description of the positronium setup used in the measurement. Positronium atoms are created from positrons (emitted from the $^{22}\text{Na}$ isotope) and electrons from the porous polymer XAD4. The polymer was placed inside the annihilation chamber around a $^{22}\text{Na}$ source with activity of 1 MBq, wrapped in a 8 µm thin Kapton foil, as indicated in Fig. 2. The annihilation chamber was installed in the centre of the J-PET detector as can be seen in the photograph in the left panel of Fig. 1. The air was pumped out of the polymer, and during the measurement the pressure in the annihilation chamber was sustained at the level of 10 Pa. The XAD4 polymer was chosen as a positronium production medium since it is characterized by a high fraction of positron-electron decays into three photons, $f_{3\gamma} = 28.9\%$.

The right panel of Fig. 1 shows an example of an event in which the three photons from o-Ps annihilation, as well as the de-excitation photon from the $^{22}\text{Na}$ source were registered. Exclusive measurements of the interaction’s position (and hence relative angles) of the three annihilation photons enable one to reconstruct the full event’s kinematics (momenta of all photons) [21]. The additional measurement of the de-excitation photon from the $^{22}\text{Na}$ decay chain ($^{22}\text{Na} \rightarrow ^{22}\text{Ne}^* e^+ \nu \rightarrow ^{22}\text{Ne} \gamma e^+ \nu$) allows one to determine the lifetime of the positronium atom. However, the finite geometrical acceptance and detection efficiency of the J-PET
Table 1: Different types of observed events. Arrows denote registered annihilation photons (solid red), not registered annihilation photons (dashed gray), and deexcitation photon (dotted blue).

|   | (I) | (II) | (III) |
|---|-----|------|-------|
|   | Annihilation into 3 photons | Annihilation into 2 photons |

detector, and the multiple Compton scatterings, also mean that there are many other possible event types with a similar signature. Therefore we need sophisticated selection procedures that we describe in the next section.

In order to estimate the influence of various background sources that could survive selection procedures, Monte Carlo simulations were preformed for the experimental setup described above. Simulations were done with dedicated software for the J-PET detector [21, 44, 45], and analysed using the same analysis procedure as for the experimental data. The positron lifetime distribution for the XAD4 material was assumed as described in [48].

Figure 2: Scheme of the annihilation chamber with the $^{22}$Na radioactive source surrounded with XAD4 material. The chamber is connected on one side to the vacuum pump. Chamber details are published in [49].
3. Selection of o-Ps → 3γ events

The positron-electron annihilation predominantly leads to the production of two or three photons. It may proceed directly ($e^+e^- → 2\gamma(3\gamma)$) or via formation of a positronium atom ($e^+e^- → Ps → 2\gamma(3\gamma)$). When requiring registration of the de-excitation photon (needed for the determination of the positron lifetime in the XAD4 material) we may define three classes of events with one (I), two (II) or three (III) registered annihilation photons, as it is graphically depicted in Table 1. In vacuum o-Ps decays only to three photons (due to C symmetry conservation). However, in the intermolecular voids of the material it may decay also into two back-to-back photons via conversion or pick-off processes. The inclusive measurements using categories I, II are typically used both in PALS and in most of the so far conducted experiments aimed at studies of discrete symmetries.

Here we concentrated on the exclusive measurement of three photons from the o-Ps → 3γ decay, case III in Table 1. Such exclusive measurements enable one to reconstruct the full event kinematics, making all
photons’ four-momentum vectors available for the physics analysis, suppressing the physical and instrumental background. Measurement of the de-excitation photon allows one to determine the lifetime of the positron in the target, and hence to disentangle between the o-Ps decays from the direct annihilation events ($e^+e^- \rightarrow 3\gamma$), and to suppress the background originating from p-Ps $\rightarrow 2\gamma$ decays followed by the secondary scattering of photons in the detector. The latter background is illustrated in the middle and right panels of Fig. 3.

De-excitation and annihilation photons are identified based on the measured time-over-threshold (TOT) values [53] that are correlated with the energy deposition in the scintillators.

Fig. 4 shows a pictorial definition of the TOT values measured with the J-PET front-end electronics [42] (upper panel) and an example TOT spectrum with superimposed regions used for the identification of the de-excitation and annihilation photons (lower panel). At each threshold (80 mV, 160 mV, 240 mV, 320 mV) a TOT$_{\text{thr}}$ value is obtained, and the TOT value is calculated as a sum of these TOT$_{\text{thr}}$. Using four threshold values for estimation of the TOT allows for a better estimation of the signal charge. It was shown that the TOT value as in Fig. 4 is a good estimator of the deposited energy [53]. The first level of reduction
of background from rescattering (middle and right panel of Fig. 3), from accidental coincidences and from cosmic rays, was applied as a condition on the distance between the decay plane and the annihilation position, as well as the time difference between the interaction of the annihilation photons’ candidates ($\Delta t_{a13}$). Due to momentum conservation, momentum vectors of the photons from the $o$-Ps $\rightarrow 3\gamma$ decay form a plane, subsequently referred to as the decay plane. In the ideal case the decay plane constructed from the measured interaction points should comprise the annihilation point. Therefore, for the $o$-Ps $\rightarrow 3\gamma$ events, the distance between the decay plane and the centre of the annihilation chamber should be close to zero, while this distance for the background events may spread even up to the radius of the detector, as shown in the upper panel of Fig. 5. Similarly, the reconstructed value of $\Delta t_{a13}$ should be close to zero in the case of the true $o$-Ps $\rightarrow 3\gamma$ process, where $\Delta t_{a13} = |t_{a3} - t_{a1}|$ with $t_{a3}$ - the largest time of registration, and $t_{a1}$ - the smallest time, out of the three determined emission times of the annihilation photons candidates. In the case of the double scattering (right panel of Fig. 3) $\Delta t_{a13}$ may reach a value of about 6 ns and for accidental coincidences it forms a continuous flat distribution as can be seen in the lower panel of Fig. 5.

Further, at the next stage of the background reduction and identification of the $o$-Ps $\rightarrow 3\gamma$ events, the angular correlation presented in Fig. 6 is used. The most pronounced single-scattered background events (middle panel of Fig. 3) form a band at 180 degrees, while the double-scattered background events (right panel of Fig. 3) are concentrated predominantly at the left side of this band. For the true $o$-Ps $\rightarrow 3\gamma$ decays, due to the momentum conservation, the sum of the two smallest relative angles defined in Fig. 3 is larger than 180 degrees and the distribution has the maximum for the symmetric configuration with the sum of relative angles equal to 240 degrees [3, 21]. In Fig. 6 (left panel) which shows experimental data obtained with the J-PET detector, such enhancement is clearly visible as expected. In order to suppress the background originating from the back-to-back photons, it is required that the sum of two smallest angles is larger than 190 degrees. Further, as the last stage of the selection, a lifetime histogram is used.

Fig. 6 presents our main result, the lifetime spectrum for $3\gamma$ events candidates meeting all of the selection criteria described. The signal from $o$-Ps $\rightarrow 3\gamma$ process is seen as a clear exponential decay with the mean lifetime of $90.2 \pm 3.5$ ns consistent with the value of $90.8 \pm 1.2$ ns expected for the mean lifetime of ortho-positronium in the used XAD4 porous polymer [48]. In addition, the production intensity of the $o$-Ps component (fraction of the $o$-Ps $3\gamma$ decays in the distribution $\rightarrow$ signal from $3\gamma$) is in agreement between the experiment ($52.8 \pm 1.5\%$) and the predictions ($53.7 \pm 3.1\%$). The predictions were made on the basis of simulations that included different fractions of positron-electron decays in XAD4 [48], detectors acceptance and analysis stream. This spectrum enables one to reject the background from direct $e^+e^- \rightarrow 3\gamma$ annihilation,
for which the lifetime is equal to about 0.5 ns [48]. Also the remaining background from the cosmic radiation and the scatterings in the annihilation chamber concentrates within few nanoseconds around zero (the maximum time needed for cosmic ray to pass through the detector). Fraction of the cosmic rays was estimated based on the separate measurement and it was equal to 1%. Taking into account corrected intensity value given above, cosmic rays can explain possible differences between simulations and experiment.

The flat distribution below the o-Ps lifetime spectrum for the negative lifetime values corresponds to the background events due to the accidental coincidences [43]. This feature enables one to estimate statistically the contribution from the accidental coincidences to the distributions which will be used for the physics studies (such as e.g. Dalitz plot distribution of the o-Ps → 3γ process). For the spectrum shown in Fig. 6 based on the simulation we can distinguish different fractions of events: clean events coming from the o-Ps annihilation into 3γ (43.01%); events in which we observe scattering of one of three annihilation photons (25.06%); events in which one annihilation hit is mistaken with hit coming from the scattering of the de-excitation photon (1.69%); events in which we register positron annihilation into 2γ with one additional scattering of annihilation or de-excitation photon (22.41%); mixed event of different annihilations (7.82%).

Figure 6: (Left panel) Distribution of the difference versus sum of the two smallest relative angles between reconstructed momentum vectors of the three annihilation photon candidates for the experimental data. The most pronounced vertical band at 180 degrees corresponds to events with annihilations into two back-to-back photons with additional scattering of one of them (middle panel of Fig. 3). Events on the left side of this band correspond predominantly to the double scattering (right panel of Fig. 3) and the signal from o-Ps → 3γ process is visible as an enhancement indicated by an arrow. (Right panel) Positron lifetime distribution determined for events that passed selection criteria for experimental data. The lifetime was calculated as the difference between the mean time of the emission of annihilation photons and the time of the emission of the de-excitation photon. Red line indicates fit to the data.

4. Conclusions

In this article we have shown that the J-PET tomography system constructed solely from plastic scintillator detectors is capable of exclusive measurements of the decays of ortho-positronium atoms. The elaborated
Figure 7: Comparison of the positron lifetime spectrum between the experiment (black line) and the simulations. Simulation spectrum was divided into different components with different origins: annihilations of positron-electron into 3 photons (red line), events in which one or more annihilation hit was coming from the scattering of the deexcitation photon (green line), annihilations of positron-electron into 2 photons with scattering of the deexcitation photon (blue line), and the mix of the different decays and more complicated scatterings containing secondary particles (cyan line). Experimental spectrum was normalized to the simulations. Possible discrepancies between the experimental data and the simulations (at the peak around zero) can be explained by the cosmic ray background. From a separate measurement, the effect of cosmic rays was estimated at about 1%.

In addition, based on the Monte Carlo simulations we have estimated various background sources, that can survive selection procedure, which allows to properly correct the lifetime distribution. The presented results, such as shown in Fig. 7, demonstrate that J-PET detector enables one to register o-Ps decays into 3 photons and to disentangle these decays from the background processes. Proper use of selection criteria may allow the simultaneous study of other types of positronium decays. With the detector performance established here, the J-PET detector provides a new tool for fundamental physics studies of positronium decays [20], for positron annihilation lifetime spectroscopy, and for entanglement studies [34, 35]. Information about the positronium lifetime in biological materials could also open a new perspective for application of positronium as a diagnostic biomarker for medicine [11, 12, 30, 33].

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References

[1] P. Moskal et al., Nucl. Instrum. Meth. A 764 (2014) 317.
[2] P. Moskal et al., Nucl. Instrum. Meth. A 775 (2015) 54.
[3] A. P. Mills and S. Berko, Phys. Rev. Lett. 18 (1967) 420.
[4] J. Yang et al., Phys. Rev. A 54 (1996) 1952.
[5] P. A. Vetter and S. J. Freedman, Phys. Rev. A 66 (2002) 052505.
[6] T. Yamazaki, T. Namba, S. Asai and T. Kobayashi, Phys. Rev. Lett. 104 (2010) 083401; Erratum: [Phys. Rev. Lett. 120 (2018) 239902].
[7] M. Skalsey and J. Van House, Phys. Rev. Lett. 67 (1991) 1993.
[8] B.K. Arbic et al., Phys. Rev. A 37 (1988) 3189.
[9] P. A. Vetter and S. J. Freedman, Phys. Rev. Lett. 91 (2003) 263401.
[10] W. Bernreuther, U. Low, J. P. Ma and O. Nachtmann, Z. Phys. C 41 (1988) 143.
[11] P. Moskal et al., Phys. Med. Biol. 64 5 (2019) 055017.
[12] P. Moskal and E.L. Stepień, PET Clinics 15 (2020) 439.
[13] S. Vandenberghhe, P. Moskal, J. Karp, EJNMMI Phys. 7 (2020) 35.
[14] P. J. Slomka, T. Pan and G. Germano, Semin. Nucl. Med., vol. 46 (2016) 5.
[15] R.D. Badawi et al., J. Nucl. Med. 60(3) (2019) 299.
[16] J.S. Karp et al., J. Nucl. Med. 61(1) (2020) 136.
[17] P. Moskal et al., Phys. Med. Biol. 61 (2016) 2025.
[18] Sz. Niedźwiecki et al., Acta Phys. Polon. B 48 (2017) 1567.
[19] P. Kowalski et al., Phys. Med. Biol. 63 (2018) 165008.
[20] P. Moskal et al., Acta Phys. Polon. B 47 (2016) 509.
[21] D. Kamińska et al., Eur. Phys. J. C 76 (2016) 445.
[22] P. Moskal et al., Eur. Phys. J. C 78 (2018) 970.
[23] D. B. Cassidy, Eur. Phys. J. D 72 (2018) 53.
[24] S. D. Bass, Acta Phys. Polon. B 50 (2019) 1319.
[25] G. S. Adkins, R. N. Fell and J. Sapirstein, Ann. Phys. 295 (2002) 136.
[26] N. Krawczyk et al., Hyperfine Interact 240 (2019) 81.
[27] W. Krzemień, E. Pérez del Río, K. Kacmanzak Acta Phys. Pol. B 51 (2020) 165.
[28] C. Vigo, L. Gerchow, L. Liszkay, A. Rubbia and P. Crivelli, Phys. Rev. D 97 (2018) 092008.
[29] C. Vigo et al., Phys. Rev. Lett. 124 (2020) 101803.
[30] P. Moskal, B. Jasیiska, E.L. Stepieі and S.D. Bass, Nat. Rev. Phys. 1 (2019) 527.
[31] Z. Bura et al., Acta Phys. Polon. B 51 (2020) 377.
[32] B. Jasіiska et al., Acta Phys. Polon. A 132 (2017) 1556.
[33] P. Moskal et al., EJNMMI Phys. 7 (2020) 44.
[34] B.C. Hiesmayr, P. Moskal, Sci. Rep. 7 (2017) 15349.
[35] B.C. Hiesmayr, P. Moskal, Sci. Rep. 9 (2019) 8166.
[36] J.N. Sun, Y.F. Hu, W.E. Frieze, D.W. Gidley, Radiation Physics and Chemistry 68 (2003) 345.
[37] Y. Kobayashi, K. Ito, T. Oka, K. Hirata, Radiation Physics and Chemistry 76 (2007) 224.
[38] https://eljentechnology.com, Plastic scintillator EJ-230.
[39] http://hamamatsu.com, Photomultiplier tube R9800s.
[40] N.G. Sharma et al., IEEE Transactions on Radiation and Plasma Medical Sciences, Vol. 4, No. 5 (2020) 528.
[41] L. Raczyіski et al., Phys. Med. Biol. 62 (2017) 5076.
[42] M. Palka et al., JINST 12 (2017) P08001.
[43] G. Korcyл et al., IEEE Transactions On Medical Imaging 37 (2018) 2526.
[44] W. Krzemieі et al., Acta Phys. Polon. B 47 (2016) 561.
[45] W. Krzemieі et al., SoftwareX 11 (2020) 100487.
[46] C. Bartram, R. Henning, D. Primosch, Nuclear Inst. and Methods in Physics Research A 966 (2020) 163856.
[47] https://www.sigmaaldrich.com, CAS Number 37380-42-0.
[48] B. Jasіiska et al., Acta Phys. Polon. B 47 (2016) 453.
[49] M. Gorgol et al., Acta Phys. Pol. B 51 (2020) 293.
[50] P.V. Stepanov et al., Phys. Chem. Chem. Phys. 22 (2020) 5123.
[51] R.L. Garwin, Phys. Rev. 91 (1953) 1571.
[52] Y.C. Jean, P.E. Mallon and D.M. Schrader, Principles and Applications of Positron and Positronium Chemistry (World Scientific, 2003) 1.
[53] S. Sharma et al., EJNMMI Physics (2020) 7.