The relationship between aortic baroreceptor activity and arterial pressure is not monotonic

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Abstract Previous reports indicate that when aortic pressure (AP) falls below the threshold ($P_{th}$) for baroreceptor sensitivity, activity in the aortic depressor nerve (ADN) may increase. To quantify and explain this anomalous behaviour, we analysed curves describing the relationship of baroreceptor fibre activity in rabbit left ADN to AP. Data were obtained in anaesthetised New Zealand White rabbits. Occlusion and release of cuffs around the inferior vena cava and descending aorta generated AP ramps (25–140 mmHg). Response curves were obtained for 173 fibres in 26 animals. Thirty percent of curves had a nadir (J-shaped curve), and in 40% activity was always present. In fibres showing activity below $P_{th}$, firing was predominantly diastolic, switching to systolic firing at $P_{th}$. The unusual behaviour of a substantial fraction of aortic baroreceptors below $P_{th}$ accounts for the J-shaped response curve of the whole ADN. We suggest that fibres that fire during diastole at pressures below $P_{th}$ may have sensory endings close to the origin of the left subclavian artery. As a consequence of this anatomical location, low pressures can impose strain on these receptors, which is then relieved by the systolic pulse.

Keywords Baroreceptor · Baroreflex · Aortic arch

Introduction

The arterial baroreceptors and their associated afferent fibres provide the sensory arm of the first order baroreflex control of arterial pressure. Stress and strain in the wall of the artery are determined by the arterial pressure, and it is these variables that are monitored by the baroreceptors. Circumferential distortion of the vessel, which occurs at lower and mid-range arterial pressures, is reported primarily by baroreceptors coupled to myelinated afferent fibres (A-fibre baroreceptors) [1–7]. Baroreceptors coupled to unmyelinated afferent fibres (C-fibre baroreceptors) appear to respond primarily to compression of the arterial wall [8] and report arterial pressure in the middle and higher range of pressure [9–12]. In combination, signals from A- and C-fibre baroreceptors will relay information about the wide range of daily arterial pressures to central nervous structures.

One might expect that the mechanical distortion of the arterial wall responsible for the activation of both A- and C-fibre baroreceptors would increase progressively as arterial pressure increases, and thus result in a monotonic relationship (response curve) between baroreceptor activity and mean arterial pressure (MAP). However, we have reported that the relationship between multifibre activity in the rabbit aortic depressor nerve (ADN) and MAP is not monotonic but assumes a ‘J-shape’ (Fig. 1 in [13]). Baroreceptor activity was monitored during slow ramps of MAP extending from 25 to 140 mmHg. There was always activity at the lowest pressure, and activity decreased as pressure was raised until a threshold pressure ($P_{th}$) was reached; above $P_{th}$, activity increased monotonically. As far as we aware there has been no other report that the baroreceptor response curve from the intact ADN assumes this shape. We have also recorded activity from single...
fibres, and some of these possessed J-shaped response curves with a nadir at \(P_{th}\) [13]. Thus the J-shaped multifibre response curve may be attributable, at least in part, to the behaviour of a substantial subpopulation of aortic baroreceptors within the ADN [13]. Indeed, there are limited reports of fibres possessing these appropriate firing characteristics [2, 3, 11].

In an attempt to explain the basis of the J-shaped response curves seen in multifibre preparations of the ADN we have re-analysed data obtained in two sets of experiments, termed series 1 and series 2. Series 1 data were obtained ~10 years prior to series 2. Using series 1 data, we re-examined the response curves of a large set of individual baroreceptor fibres, describing and quantifying their behaviour at lower pressures. Based on the presence or absence of silence and/or a nadir at lower pressures, we identified and quantified four different types of response curve. Using series 2 data, we investigated the basis of the frequent anomalous behaviour of baroreceptors at lower pressures. We measured pressure in the aortic arch using a catheter-tip manometer. In some instances we obtained simultaneous recordings of aortic diameter. Collectively, these measurements allowed us to propose an explanation for the non-monotonic, J-shaped response curve of a substantial population of aortic baroreceptors.

**Methods**

**Ethics approval**

The experimental procedures were approved by the Committee on Ethics in the Care and Use of Laboratory Animals, University of Otago.

**Animals**

Both series of experiments were performed using adult New Zealand White rabbits of either sex (2.2–5.0 kg).

**Preparations**

**Series 1** Animals were anaesthetised with 30–40 mg kg\(^{-1}\) sodium pentobarbitone i.v. in an ear vein. Further anaesthetic was administered as required. Mechanical ventilation was applied through a tracheal cannula, and colonic temperature was maintained at 37–38°C. A short catheter was advanced to the aortic arch through the left brachial artery, and aortic pressure (AP) was measured with a Statham P23DC pressure transducer (Hato Rey, Puerto Rico).

**Series 2** Animals were anaesthetised with chloralose (50 mg kg\(^{-1}\) i.v.) and urethane (1 g kg\(^{-1}\)), with further anaesthetic administered as required. Animals were maintained as described for series 1. A 3F catheter-tip manometer (SPR-249, Millar Instruments, Houston, TX, USA) was inserted into the right femoral artery and advanced to the aortic arch. In some preparations, ultrasonic crystals (5 MHz, 2-mm diameter; Triton Technology, San Diego, CA, USA) were placed on the descending thoracic aorta 4–5 cm caudal to the apex of the aortic arch, and aortic diameter (\(D_{ao}\)) was measured using a sonomicrometer (Triton Technology, Model 6).

**Generating ramps of systemic arterial pressure**

The chest was opened between the fourth and fifth ribs and end-expiratory pressure was set at 3–5 cmH\(_2\)O. Perivascular cuffs (5-mm diameter; In Vivo Metric, Healdsburg, CA, USA) were secured around the inferior vena cava and the descending thoracic aorta. Inflation and deflation of the inferior vena cava cuff followed by inflation of the aortic cuff generated pressure ramps that rose from ~25 to ~140 mmHg (at 0.5–1.0 mmHg s\(^{-1}\) in series 1, and ~2 mmHg s\(^{-1}\) in series 2).

**Recording baroreceptor activity**

The left ADN was exposed in the neck and cut at its junction with the superior laryngeal nerve. For recording multifibre activity, the intact ADN was placed on a pair of platinum electrodes and embedded in a fast-curing silicone gel (Wacker SilGel 604, Wacker-Chemie, Munich, Germany). At least 30 min elapsed before data were collected. To record single fibre baroreceptor activity, the ADN was split into small filaments. Individual filaments were placed over one electrode with the indifferent electrode grounded to the surrounding tissue through a fine cotton thread. Filaments were split repeatedly until the signal from a single afferent fibre was discriminable. Signals from nerve preparations were amplified (Model P15D, Grass Instruments, Quincy, MA, USA and DAM80, World Precision Instruments, Sarasota, FL, USA, for series 1 and series 2 data respectively), and filtered (high and low pass filters: 100 Hz and 3 kHz for multifibre preparations, and 100 Hz and 3 kHz for single fibre preparations).

**Data acquisition and analysis**

**Series 1** Analogue signals of nerve activity and AP were digitized (Vetter PCM, Model 3000A, Rebersburg, PA, USA) and stored on videotape. The tape was replayed and signals appropriately treated prior to recording as a Chart file (Chart 3.4, ADInstruments, Castle Hill, NSW, Australia) from which the data were extracted. Action potential frequency was obtained by passing the electroneurogram
through a custom-made discriminator and counter. Action potentials were counted in 0.2-s bins. For multifibre activity the threshold of the discriminator was set just above the noise level recorded after the AP cuff was deflated at the end of a pressure ramp, when nerve activity was briefly absent.

Series 2  Data were recorded and processed using software in Chart v5.5.6 (ADInstruments). The firing frequency of individual action potentials was obtained from the raw baroreceptor signal using the cyclic variable software. Each recording was inspected closely in order to describe the mechanical events associated with the firing of action potentials.

Results

Series 1: multifibre baroreceptor recording

Figure 1a–f shows examples of response curves from six different preparations randomly selected from 30 similar records obtained over a 3-year period. Each panel shows a single unfitted response curve to a pressure ramp. All response curves are non-monotonic, possessing a J-shape with a nadir in the region of 40–55 mmHg. In all examples there is significant nerve activity at low pressures. All 30 preparations had response curves that conformed to this general pattern. A curve that presents the mean of the individual responses is not presented since it would tend to blur the nadir and shape of the response curve at lower pressures.

Series 1: single fibre baroreceptor recording

Recordings were obtained from 173 separate single baroreceptor fibres in 26 animals. Initial examination of response curves from these fibres suggested that they could be described using a minimum of four categories. This allowed responses to be grouped by two distinct characteristics (Fig. 2). The first characteristic concerns the nature of the pressure-activity relationship—either monotonic or non-monotonic (a J-shape showing a nadir). The second characteristic was the absence or presence of silence (a pressure/pressure range over which a fibre did not fire). Every fibre was placed in a category (types A–D) based on these two response characteristics. For every fibre we quantified five variables. These were the threshold pressure \( P_{th} \) at which activity began to increase with increasing pressure, and the firing rate at this threshold \( F_{th} \); the pressure \( P_{max} \) at which activity reached a maximum \( F_{max} \); and gain \( G \) as the ratio \( (F_{max} - F_{th})/(P_{max} - P_{th}) \). Values of these variables for the four different fibre types were compared using ANOVA followed by Fisher’s LSD.

Table 1 shows the categorical distribution of fibres and the values of five measured variables. Almost 50% of fibres (type A) had a ‘classic’ sigmoidal response curve with silence below \( P_{th} \). Over half the total population did not respond in this manner; curves from 30% of the fibres demonstrated a nadir (Fig. 3a; types C and D), and 40% were never silent over the ramp pressure range (Fig. 3a; types B and D). The features possessed by types A–D most likely explain the overall shape of the multifibre response curves (Fig. 1), which have a nadir and show activity at all pressures tested. Fibres of type B (sigmoidal response curve with no silence at \( P_{th} \)) had a significantly higher maximum firing rate than the other three fibre types \((P < 0.01)\). Type D fibres (nadir in the response curve with no silence at \( P_{th} \)) had lower gain than either type A or C \((P < 0.01)\). It should be noted that since the pulse characteristics were not controlled, values for \( P_{th} \) and \( P_{max} \) are...
not necessarily comparable with those from other studies. On the other hand, our data do reflect natural responses, and we have assumed that variability in pulse characteristics occurred randomly.

Since the fibres were randomly selected and the sample size was substantial, we considered that the distribution of fibres within the categories, summarised in Table 1, was a reasonable representation of their sampling within a multifibre recording. To see how this multifibre recording might appear, we assembled the responses of the 173 fibres to generate a response curve for a ‘multifibre’ recording of baroreceptor A-fibres (Fig. 3b). The assembled curve (ALL) possesses the two key features seen in the multifibre response curves in Fig. 1—activity present at all pressures and a nadir at $P_{th}$.

Series 2: single fibre baroreceptor recording

Using this series of response curves we examined the detailed behaviour of individual baroreceptor fibres during a pressure ramp. The purpose was to examine the relationship between fibre activity and the features of AP in an

![Fig. 2](image)

**Table 1** Characteristics and population distribution of the four types of baroreceptor fibres classified by their response curves (see Fig. 2)

| Type   | Number | Percentage | $P_{th}$ (mmHg) | $F_{th}$ (Hz) | $P_{max}$ (mmHg) | $F_{max}$ (Hz) | Gain (Hz/mmHg) |
|--------|--------|------------|-----------------|-------------|-----------------|---------------|----------------|
| A      | 83     | 48         | 52 ± 10         | 0           | 130 ± 13        | 59 ± 22       | 0.76 ± 0.28    |
| B      | 38     | 22         | 54 ± 16         | 13 ± 13$^*$ | 135 ± 12        | 71 ± 21$^*$   | 0.72 ± 0.29    |
| C      | 20     | 12         | 54 ± 12         | 0           | 133 ± 9         | 60 ± 23       | 0.76 ± 0.29    |
| D      | 32     | 18         | 56 ± 12         | 22 ± 16$^{1,3}$ | 132 ± 12       | 62 ± 17       | 0.54 ± 0.21$^{**}$ |
| Never silent (B and D) | 70 | 40 | | | | |
| Display nadir (C and D) | 52 | 30 | | | | |
| Total/mean | 173 | 54 ± 12 | 7 ± 13 | 132 ± 12 | 63 ± 21 | 0.7 ± 0.3 |

Primary features of response curves of aortic baroreceptor fibres from the left ADN, grouped (types A, B, C, D; see Fig. 2). Values for fibre characteristics are presented as the mean ± SD

- $P_{th}$ Pressure threshold at which activity increases,
- $F_{th}$ firing rate at $P_{th}$,
- $P_{max}$ pressure at which firing rate reaches a maximum,
- $F_{max}$ maximum firing rate,
- gain mean slope of the response curve between $P_{th}$ and $P_{max}$

$^*$ Significantly different from A; $P < 0.01$

$^{**}$ Significantly different from A, B and C; $P < 0.01$

$^1$ Significantly different from A and C; $P < 0.01$

$^{3}$ Significantly different from B; $P < 0.05$
attempt to explain the shape of the response curves and, in particular, the basis of the non-monotonic J-shaped response. Data were obtained from 13 animals. Multifibre recordings of the intact ADN were made prior to nerve splitting. All the multifibre records yielded J-type response curves when activity was measured as either the frequency of individual action potentials (as performed for series 1) or as integrated activity. We obtained recordings from 120 single baroreceptor fibres during pressure ramps, and 44 of these (37%) possessed J-shaped response curves and were designated either type C or D; a similar proportion of series 1 fibres (30%) fell into these two categories (Table 1).

Figure 4a, b shows the ramp responses of one type A and one type B fibre, having monotonic response curves. Both recordings were obtained in the same animal. At the lowest APs, well below $P_{th}$, the type B fibre was firing at about 50% of $F_{max}$ ($F_{th} \approx 30$ Hz). Firing frequency was relatively constant throughout a cardiac cycle with a small decline coincident with early systole. A small but pronounced increase in systolic firing appeared at $P_{th}$, which became larger as pressure was raised further. At moderate APs, the pressure pulse produced large fluctuations in aortic diameter ($D_{ao}$), with a large positive $dD_{ao}/dt$. At higher APs the aorta was stiffer, and even though pulse pressure was increasing, the pulsatile variations in $D_{ao}$ and $dD_{ao}/dt$ were much reduced. In all fibre types, reductions in peak positive $dD_{ao}/dt$ and in the amplitude of fluctuations of $D_{ao}$ were associated with an increase in diastolic firing.

A response from a type D fibre is shown in Fig. 5. At the lowest pressures firing was entirely diastolic with up to seven action potentials per cycle, but as the nadir of the response curve was approached, firing rate was reduced to a single action potential during early systole. Above $P_{th}$ the behaviour of this fibre was indistinguishable from types A–C; initially there was an increase in systolic firing, while at higher pressures diastolic firing entered the record. Many type D fibres had a higher discharge rate at the nadir than the example in Fig. 5, such that the mean discharge for type D fibres at $P_{th}$ was 22 ± 16 Hz. There was considerable variation in $P_{th}$ for all fibre types. As an example this is evident in the recording of two type D fibres in Fig. 6, where $P_{th}$ for the fibre with larger amplitude signal occurs ~20 mmHg below the $P_{th}$ for the fibre with the smaller signal. The behaviour of both of these fibres at low pressures matches the description given for the fibre shown in Fig. 6. Indeed, all type C and type D fibres showed similar subthreshold behaviour, with firing at the lowest pressures usually restricted to diastole. The differences between type D and type C fibres were that type C was silent at the nadir and had higher gain (Table 1).

We used ramps of increasing pressure to examine the discharge characteristics of the baroreceptors. It is well established that response curves based on ramps of decreasing pressure demonstrate hysteresis, and a higher value for $P_{th}$ is observed on the descending limb of a ramp. To see whether the direction of pressure change affected the discharge pattern of type C and D fibres, we examined our records for ramps of descending pressure. We had not intended to perform descending ramps, so we searched the records for sections where a steady decline in AP occurred at the time when the cuff around the inferior vena cava was inflated to initiate an ascending ramp. An example of one of these descending ramps and the following ascending
As expected [11], $P_{th}$ was higher in the descending ramp than in the ascending ramp ($\sim 10 \text{ mmHg}$). Significantly, the J-shape response curve of this fibre was apparent in both ascending and descending ramps. In the descending ramp the fibre was silent for several cycles when switching from systolic to diastolic firing, indicating that this feature as well as $P_{th}$ is sensitive to the direction of the pressure ramp.

**Discussion**

As far we are aware, this is the first systematic exploration and quantification of the behaviour of aortic baroreceptors at low APs. While the presence of activity in aortic baroreceptors at low pressures has been reported previously [2, 3, 11], there is no report that has quantified or explained this behaviour at low pressure. We have now demonstrated that approximately one-third of the aortic baroreceptors in the rabbit have a non-monotonic J-shaped response curve. In addition we found that 40% of all fibres were not silent at subthreshold pressures (termed autoactive fibres by Munch [3]), and these included $>30\%$ of all fibres possessing a sigmoidal response curve. When we pooled the response curves of all fibres sampled, the result resembled a multifibre curve with a distinct J-shape and substantial firing at low APs (Fig. 3b). The behaviour of the various fibre types at pressures above $P_{th}$ was quite similar (Table 1). This suggests that a basis for the differences in their behaviour below $P_{th}$ may be attributable to their location within the barosensory region innervated by the left ADN.

Others have reported the presence of baroreceptor activity at subthreshold pressures. In a study on the in situ preparation of the rabbit aortic arch, Angell James [2] reported that 6 of 26 single fibres from the left ADN showed constant activity over a range of 20–40 mmHg below $P_{th}$, and as pressure rose activity ‘even diminished’ before $P_{th}$ was reached. In the same study, the importance of longitudinal strain and the tethering effect of the arteries and aorta on the discharge of aortic baroreceptors was noted. When recordings were made on in vitro preparations of the aortic arch, only 1 fibre out 31 fired at pressures below $P_{th}$. All of these data were obtained using a non-pulsatile pressure, so any significance of a change in strain during a pressure pulse could not have been detected. Our records (Figs. 4b, 5, 6, 7) show that the majority of firing at subthreshold pressures in type C and D fibres (J-shaped response curves) occurs during diastole. Indeed, the rising phase of systole appears to turn off firing, a reverse of the
situation that occurs once $P_{th}$ is reached. Likewise, type B fibres that fired at a steady mean frequency at pressures below $P_{th}$ usually demonstrated a small reduction in instantaneous firing rate at the onset of the pressure pulse. Thus it appears that lower pressures may increase strain at particular locations within the barosensory area and that this strain can be temporarily relieved by the rise in pressure in early systole.

The discrete diastolic firing pattern seen in type C and D fibres occurs at values of AP where the aorta is above its unstressed volume (e.g. $\sim 60/40$ mmHg, see examples in Figs. 6, 7). It is difficult to see how falling pressure during diastole could generate an increase in circumferential strain and load baroreceptor endings within the wall of a stressed vessel. On the other hand, this baroreceptor firing pattern may be explained by the anatomy of the outer curvature of the aortic arch. Several major arterial vessels arise from the outer curvature of the arch, and baroreceptors with afferents located in both the right and left ADN are located at the origin of these arterial vessels. A reduction in pressure may increase longitudinal strain at these locations, and this strain may then be temporarily relieved by the rise in pressure in systole. Feng and colleagues [14] have examined these ideas in a theoretical and electrophysiological investigation of the axial (longitudinal) and circumferential strain in the rat aortic arch. They found that the relationship between axial strain and AP displayed a U-shape, with its minimum in the region of 70–100 mmHg. When pressure was reduced below this minimum, axial strain increased. We propose that the mechanical behaviour of the aortic arch and the response of the baroreceptors occur as follows: at lower pressures the outer curvature of the aorta will move inwards, but this movement will be opposed by the subclavian and brachiocephalic arteries that are anchored to and tether the outer curvature of the aortic arch. Baroreceptors close to the origin of the two large arteries would be subjected to increasing axial strain when pressure fell during diastole, while the rising systolic pulse
Fig. 6 Record of two type D baroreceptors. The frequency of the larger unit is shown in the bottom trace. At low pressures (left of A) both receptors fired during diastole. At A, the larger unit began firing during systole, while the smaller unit continued to fire during diastole. $P_{th}$ for the larger unit is the pressure at A, while $P_{th}$ for the smaller unit is the pressure at B. From their respective $P_{th}$ values each fibre showed an increase in firing rate with increasing pressure. The mean discharge for the larger unit was identical at the lowest and highest pressures shown in this figure (six action potentials per cycle).

Fig. 7 Responses of a type D baroreceptor to ramps of decreasing and increasing aortic pressure. The ramps encompass baseline control and lower pressures and were obtained by gradual inflation followed by gradual deflation of a cuff around the inferior vena cava. At higher pressures in both ramps firing occurs in systole, while at lower pressures it occurs during diastole. In comparison to responses to increasing pressure, with falling pressure the baroreceptor activity tended to be lower at any particular pressure and became silent when switching between the two firing modes. All our measurements and classifications in this paper were made on ramps of increasing pressure, thus we categorised this fibre as type D rather than type C.
would relieve the strain. The two baroreceptor fibres illustrated in Fig. 6 altered their firing patterns at quite different pressures. On a ramp of rising pressure, a switch from diastolic firing to systolic firing in the fibre with the larger amplitude signal occurred (at A) at a pressure ~15 mmHg lower than for the fibre with the smaller signal (switch at B). Differences in the AP at which switching occurs may be explained by differences in location of the baroreceptor endings and the potential influence of tethering in their localities.

In our study we did not identify the anatomical locations of the baroreceptor terminals associated with type C and D fibres. This would have required substantial dissection in the region of the aortic arch. As discussed below, we intentionally avoided disturbing the aortic arch in order to observe responses that were as close to natural as possible. It may be possible to identify the location of type C and D receptors using tactile stimuli [15, 16] in a preparation that has undergone further dissection but which leaves the aortic arch and the subclavian and brachiocephalic arteries relatively undisturbed.

We would expect to find a similar relationship between the distribution of wall strain and pressure in the aortic arch of other mammals, including humans. Pelletier et al. [11] described the response curves of carotid and aortic receptors in dogs to pulsatile pressure ramps and presented the response curves for four individual aortic baroreceptors (their Fig. 8). Two of the curves had a distinct J-shape, but this is not discussed in their paper. Similar responses have been recorded from baroreceptors located in other barosensory regions. Angell James [2] found that 2 of 10 baroreceptor fibres from the brachiocephalic region of the rabbit fired regularly at pressures below $P_{th}$.

An important feature of the present study is that the data were obtained under conditions where the aortic arch was exposed to flowing blood and pulsatile pressure fluctuations that were essentially natural. While these conditions meant that there was some variation in the pulsatile pressure pulse between preparations and during a pressure ramp procedure, the collected data will resemble signals that would occur under normal auto-perfused conditions. These conditions contrast with those of many published studies in which unnatural conditions involving pulse-free ramps, no-flow preparations, or physiological solutions replacing blood provide very reliable experimental protocols and analysis, but yield data from which extrapolation to in vivo behaviour is considerably more difficult.

We have argued that the non-monotonic response curve obtained from aortic baroreceptors possessing type C and D response curves is a consequence of the anatomy of the outer curvature of the aorta arch and associated arterial branches. The behaviour of these baroreceptors at low arterial pressure can be considered a default of the anatomical distribution of these receptors rather than as serving a particular function. It seems unlikely that pressures below $P_{th}$ are encountered in the normal life of a rabbit. However in the event that pressure should fall below $P_{th}$, for example as a result of a severe haemorrhage, an increase in activity from these baroreceptors may inhibit sympathetic activity and lead to an undesirable decompensation of the haemorrhagic response. This possibility is supported by observations made during collection of data to construct baroreflex response curves (relating heart rate or sympathetic nerve activity to MAP). When MAP was reduced below the $P_{th}$ seen in the present study by inflation of a cuff around the IVC, the raw data for heart rate [17, 18] or renal sympathetic nerve activity [17, 19] displayed a biphasic response that matched the response we predict. A majority of baroreflex studies present curves that have been fitted by mathematical expressions which do not allow for, and cannot expose, a biphasic response at subthreshold values for MAP (for an example see Fig. 1 in [19]). While the appearance of a biphasic reflex response at low pressure is congruent with the behaviour of aortic baroreceptor activity, it does not demonstrate causality.

Summary

At arterial pressures below the $P_{th}$ of sensitivity of aortic baroreceptors to increasing pressure, a subset of baroreceptors are active. This activity occurs primarily during diastole, and its frequency is often greater than the frequency at $P_{th}$. The activity/pressure curve for these fibres takes on a J-shape, and the same relationship between activity and pressure is evident in whole nerve multibre recordings. The behaviour of these baroreceptors at low pressure may be attributable to the longitudinal/axial strain in their vicinity, consequent to tethering of the outer curvature of the aorta by the subclavian and brachiocephalic arteries. It needs to be established whether the behaviour of this subset of baroreceptors at low pressures produces unusual baroreflex regulation of the circulation.

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