Lubricin is expressed in chondrocytes derived from osteoarthritic cartilage encapsulated in poly (ethylene glycol) diacrylate scaffold

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Abstract

Osteoarthritis (OA) is characterized by degenerative changes within joints that involved quantitative and/or qualitative alterations of cartilage and synovial fluid lubricin, a mucinous glycoprotein secreted by synovial fibroblasts and chondrocytes. Modern therapeutic methods, including tissue engineering techniques, have been used to treat mechanical damage of the articular cartilage but to date there is no specific and effective treatment. This study aimed at investigating lubricin immunohistochemical expression in cartilage explant from normal and OA patients and in cartilage constructions formed by Poly (ethylene glycol) (PEG) based hydrogels (PEG-DA) encapsulated OA chondrocytes. The expression levels of lubricin were studied by immunohistochemistry: i) in tissue explanted from OA and normal human cartilage; ii) in chondrocytes encapsulated in hydrogel PEGDA from OA and normal human cartilage. Moreover, immunocytochemical and western blot analysis were performed in monolayer cells from OA and normal cartilage. The results showed an increased expression of lubricin in explanted tissue and in monolayer cells from normal cartilage, and a decreased expression of lubricin in OA cartilage. The chondrocytes from OA cartilage after 5 weeks of culture in hydrogels (PEGDA) showed an increased expression of lubricin compared with the control cartilage. The present study demonstrated that OA chondrocytes encapsulated in PEGDA, grown in the scaffold and were able to restore lubricin biosynthesis. Thus our results suggest the possibility of applying autologous cell transplantation in conjunction with scaffold materials for repairing cartilage lesions in patients with OA to reduce at least the progression of the disease.

Introduction

Articular cartilage homeostasis is the result of an intricate interplay between anabolic and catabolic, anti- and pro-inflammatory, anti- and pro-apoptotic mediators. These processes act also as protective mechanisms whether there is a sub lethal injury characterized by an increased survival of chondrocytes, which play, in that way, a central role in the growth of the new cartilage and extracellular matrix.1,2 As chondrocytes represent versatile regulators for this cartilage equilibrium, they are highly sensitive and responsive to mechanical, biochemical and other stressful stimuli.3 However, any kind of cartilage injury can lead to an irreversible cartilage loss, since differentiated chondrocytes do not divide and hence do not compensate for these defects. Additionally, cartilage homeostasis is disturbed by the predominance of directly and indirectly catabolic acting factors such as pro-inflammatory cytokines, which can result in cartilage damage and secondary osteoarthritis (OA).4 Osteoarthritis, also known as degenerative arthritis, is a multifactorial degenerative joint disease, characterized by degenerative changes within joints that involved quantitative and/or qualitative alterations of cartilage and synovial fluid lubricin, a mucinous glycoprotein secreted by synovial fibroblasts and chondrocytes. It can be classified into either primary or secondary depending on whether there is an identifiable underlying cause or not. The progressive erosion of articular cartilage, leading to joint space narrowing, subchondral sclerosis, subchondral cyst, synovial inflammation, and marginal osteophyte formation, characterizes the disease process of OA.5 It is known that OA is the result of mechanical and biological processes that modify cartilage homeostasis.6,5

Modern therapeutic methods, including tissue engineering techniques, have been used to treat the mechanical damage of articular cartilage. Among a number of these recently developed methods, the autologous chondrocyte transplantation (ACT) seems promising. In this procedure, the chondrocytes were isolated from a cartilage, these chondrocytes are cultured in vitro, and subsequently, they can be transplanted into the damaged area. Some studies have revealed that these cells are capable of producing, in vivo, an extracellular matrix of chemical composition and biomechanical properties similar to those of normal hyaline cartilage.6,7 In this respect, chondrocytes of the middle and deep zones synthesize aggrecan at high rates, and thereby contribute to the ability of cartilage to bear compressive loads; on the other hand, the chondrocytes of the superficial zone exhibit a number of specific functions including the synthesis and secretion of superficial zone protein (SZP) also known as proteoglycan 4 (Prg4) or lubricin.

Lubricin (227.5-kDa) is a mucinous glycoprotein secreted by synovial fibroblasts and chondrocytes.8 This molecule is partly responsible for the lubrication of apposed and pressurized cartilage surfaces, enabling low friction levels.9,10 Lubricin provides essential chondroprotective properties to articular cartilage as shown by the lack of cartilage surface integrity and surface disruption in lubricin knockout mice.11 Furthermore, quantitative and/or qualitative alterations of cartilage and synovial fluid lubricin have been described in OA. Lubricin has been localized on the surface of multiple synovial tissues, including cartilage, meniscus, ligament, and tendon,12,13 whereupon it acts as a boundary lubricant and as a deterrent against abnormal protein deposition and/or cellular adhesion. In addition, lubricin contributes to the load dissipating elasticity of synovial fluid. Thus, the expression of lubricin in chondrocytes delivered on absorbable scaffolds seems to be absolutely necessary. As regards this, some studies have demonstrated that chondrocytes from the
superficial zone of bovine cartilage, used in explants, monolayer, transplant and alginate constructions are able to express lubricin. However, to the knowledge of authors, no investigation has ever dealt with lubricin expression in human autologous chondrocytes derived from normal and OA cartilage and encapsulated into scaffold. Accordingly, this study aimed at investigating lubricin immunohistochemical, immunocytochemical expression and western blot analysis in cartilage explant from normal and OA patients and in cartilage construction formed by Poly (ethylene glycol) (PEG) based hydrogels (PEG-DA) encapsulated OA chondrocytes.

Materials and Methods

Subjects

Osteoarthritic cartilage was obtained from 25 patients, 15 males and 10 females, with similar height and weight, who underwent knee joint replacement at the Orthopaedic and Traumatology Unit, Hospital of Suzzara, Mantova, Italy, under an approved Institutional Review Board protocol after obtaining the required informed consent from the patients. Surgery was performed because of the pain and the functional impairment. The median of the age of the OA patients was 56 (range 34-78 years). Tissue samples were graded according to the histopathological Mankin scores and included only pieces of moderate-to-severe OA (Mankin score 6-14). The patients were not smokers, occasionally taking NSAIDs (nonsteroidal anti-inflammatory drugs) in addition to the classical treatment for knee OA composed of hot packs, therapeutic ultrasound and steroid anti-inflammatory drugs) in addition to the classical treatment for knee OA.

Isolation of chondrocytes and culture conditions

To isolate the chondrocytes from OA and non OA articular cartilage, they were incubated in Dulbecco’s modified eagle’s medium (DMEM, Gibco, Grand Island, NY, USA) containing 0.2% collagenase (Worthington Biochemical Corporation, Lakewood, NJ, USA) and 5% FBS (fetal bovine serum, Gibco) for 14-16 h at 37°C and 5% CO₂. The resulting cell suspension was then filtered through 70 μm nylon filters (Cell Strainer, Falcon, Franklin Lakes, NJ, USA) and washed three times with phosphate buffered saline (PBS) containing 100 U/ml penicillin and 100 μg/ml streptomycin. The number and size distribution of the isolated cells were then determined with a Z2 Coulter Counter and Size Analyzer (Beckman Coulter, Inc., Palo Alto, CA, USA).

Cell encapsulation in hydrogels (PEGDA)

Cells were encapsulated in PEGDA hydrogels for 3, 4 and 5 weeks. Briefly, chondrocytes (passage 3 or 4) were suspended in 10% (w/v) PEGDA (SunBio, Orinda, CA, USA) solution in sterile PBS with 100 U/ml penicillin and 100 μg/ml streptomycin (Gibco). The photoinitiator Irgacure 2959 (Ciba Specialty Chemicals, Tarrytown, NY, USA) was used at 0.05% (w/v) final concentration. The photo initiation and encapsulation processes have been previously determined to be biocompatible. Chondrocytes were resuspended in 95 μL of polymer solution at a concentration of 2×10⁵ cells per milliliter. The cell-polymer solution was added to a cylindrical silicone-tubing mold with an internal diameter of 4.75 mm and a construct height of 5 mm. The tubing was attached to the glass microscope slide using silicon lubricant. Prepolymer (macromer) was exposed to UV light (365 nm) for 5 min to induce gelling. Constructions were removed from the molds and cultured at 37°C, 5% carbon dioxide in chondrocyte medium. The culture medium was changed twice weekly. The scaffolds were photographed with a digital camera (Canon, Tokyo, Japan).

Fixation, dehydration and embedding of hydrogels

The hydrogel was fixed by incubating it in 500 μL of 4% paraformaldehyde (w/v) in PBS (Invitrogen), pH 7.4 overnight (~12 h). Several steps involving temperature and pH changes were necessary to dissolve this chemical to dissolve the paraformaldehyde, heat the solution to 55°C while stirring. Once dissolved, 1N NaOH drop by drop was added to the solution until it became clear. Dilute HCl was used to lower the pH to 7.4. Then the hydrogel was dehydrated using the following sequence: 70% EtOH x 1 h, 80% EtOH x 1.5 h, 95% EtOH x 1 2 h, 100% EtOH x 1.5 h-repeat twice, Xylen x 1 h.

A metal mold (and embed in paraffin at 60°C overnight (~12 h). The paraffin was poured out and replaced with fresh paraffin. An embedding cassette (Fisher) was placed on top of the mold and additional paraffin was added to fill the cassette. Cooled for 1 h using the cold surface of the embedding station (the embedding system used was Leica EG1150). Sections of 5-μm thick were cut from paraffin blocks using a microtome and they were mounted on saline-coated slides and stored at room temperature.

Immunohistochemistry

For immunohistochemical analysis, sections were incubated for 30 min in 0.3% H₂O₂/methanol to quench endogenous peroxidase activity then rinsed for 20 min with phosphate-buffered saline (PBS; Bio-Optica, Milano, Italy). The sections were irradiated (5 min x 3) in capped polypropylene slide-holders with citrate buffer (pH 6), using a microwave oven (750 W) to unmask antigenic sites. Then, the sections were incubated with diluted rabbit polyclonal anti-lubricin antibody (abcam, Cambridge Science Park, Cambridge, CB4 0FL, UK), (diluted 1:50 in PBS) overnight at 4°C. The secondary antibody, biotinylated mouse/anti-rabbit IgG was applied (for 30 min at RT), followed by the avidin-biotin-peroxidase complex (Vector Elite Kit Abbott, Chicago, IL, USA) for 30 min, at room temperature. The immunoreaction was visualized by incubating the sections for 4 min in a 0.1% 3,3′-diaminobenzidine and 0.02% hydrogen peroxide solution (DAB substrate kit, Vector Laboratories, CA, USA). The sections were lightly counterstained with Mayer’s haematoxylin (Histolab Products AB, Goteborg, Sweden) mounted in GVA mount (Zymed, Laboratories Inc., San Francisco, CA, USA).
observed with an Axioplan Zeiss light microscope (Germany) and photographed with a digital camera (Canon, Japan).

**Immunocytochemistry**

Immunostaining for lubricin was performed on control and OA cell cultures in cells after fourth passages in monolayer cultured. Briefly, cells were fixed with 4% phosphate-buffered paraformaldehyde, for 20 min at room temperature; quenching was performed with a solution of 2% hydrogen peroxide (H₂O₂) and 10% methanol in phosphate-buffer saline (PBS) for 1 min. To permeabilize the cells, fresh 0.3% Triton X-100 solutions in PBS was used for 5 min. The cells were then treated with 5% bovine serum albumin (BSA) in PBS for 1 hour at room temperature. BSA is a blocking agent used to prevent non-specific binding of the antibody. After blocking, the cells were incubated overnight with a primary Rabbit anti-PRG4 unconjugated (1:200 dilution, Millipore, Billerica, MA, USA) antibody. A fluorescein isothiocyanate (FITC) labeled anti-rabbit antibody (1:100, Santa Cruz Biotechnology, Inc., Santa Cruz, CA, USA) was used as a secondary antibody. Cover slips containing the cells were washed and mounted in PBS/glycerol (50:50) and placed on glass microscope slides. In all instances negative controls without primary antibody were performed. Cover slips were analyzed using a Nikon Eclipse TE200 fluorescence microscope and photographed with a digital camera (Canon) and positive cells were counted over the entire cover slips.

**Evaluation of immunohistochemistry and immunocytochemistry**

The lubricin-staining status was identified as either negative or positive. Immunohistochemistry positive staining was defined as the presence of a brown detection chromogen on the edge of the hematoxylin-stained cell nucleus, distributed within the cytoplasm or in the immediate lacunar/pericellular space evaluated by the light microscope. Immunocytochemistry positive staining was defined as the presence of fluorescence detection on the edge of the black background, distributed within the cytoplasm or in the immediate lacunar/pericellular space evaluated by the fluorescence microscope.

Stain intensity and the proportion of immunopositive cells were assessed also by light and fluorescence microscopy. Intensity of staining (IS) was graded on a scale of 0-4, according to the following assessment: 0, no detectable staining; 1, weak staining; 2, moderate staining; 3, strong staining; 4, very strong staining. The percentage of Lubricin-1 immunopositive cells (Extent Score=ES) was independently evaluated by 3 investigators (2 anatomical morphologists and one histologist) and scored as a percentage of the final number of 100 cells in five categories: 0, <5%; +, 5-30%; ++, 31-50%; ++++, 51-75%, and ++++, >75%. Counting was performed at x200 magnification.

Positive and negative controls were performed to test the specific reaction of primary antibodies used in this study at a protein level. For positive control testing the sections and cells culture from synovium underwent an immunoperoxidase process. The positive immunolabeling for lubricin was cytoplasmic. For negative control testing sections and cells of cartilage were treated with normal rabbit serum instead of the specific antibodies.

**Western blot analysis**

The expression of lubricin was evaluated by Western blot analysis. The monolayer chondrocytes were washed twice with ice-cold PBS and collected with lysis buffer (10 mM Tris-HCl plus 10 mM KCl, 2 mM MgCl₂, 0.6 mM PMSF, and 1% SDS, pH 7.4). After cooling for 30 min at 0°C, cells were sonicated. Twenty micrograms of total protein, present in the supernatant, were loaded on each lane and separated by 4-12% Novex Bis-Tris gel electrophoresis (NuPAGE, Invitrogen, S.Giuliano Milanese, MI, Italy). Proteins were then transferred to nitrocellulose membranes (Invitrogen) in a wet system. The transfer of proteins was verified by staining the nitrocellulose membranes with Ponceau S and the Novex Bis-Tris gel with Brilliant blue R. Membranes were blocked in Tris buffered saline containing 0.01% Tween-20 (TBST) and 5% non-fat dry milk at 4°C overnight. Rabbit polyclonal lubricin (abcam, Cambridge Science Park, Cambridge, CB4 0FL, UK), 280 KD a (1:500 dilution), and mouse monoclonal anti-a-tubulin antibodies (Sigma, Milano, Italy), 50 KD a (1:5000) were diluted in TBST and membranes incubated for 24 h at room temperature. Antibodies were detected with horseradish peroxidase-conjugated secondary antibody using the enhanced chemiluminescence detection Supersignal West Pico Chemiluminescent Substrate (Pierce Chemical Co., Rockford, IL, USA). Bands were measured densitometrically and their relative density calculated based on the density of the a-tubulin bands in each sample. Values were expressed as arbitrary densitometric units (A.D.U.) corresponding to signal intensity.

Figure 1. A) Lubricin immunohistochemistry (cytoplasmic and perinuclear immunolabeling) specimen from control cartilage (tissue explanted); strong lubricin immunolabeling of chondrocytes; magnification x20; scale bar: 100 µm. B) Magnification of panel A, black arrow; magnification x40; scale bar: 50 µm. C) Magnification of panel A, red arrow; magnification x40; scale bar: 50 µm. D) Lubricin immunohistochemistry specimen from OA cartilage (tissue explanted); weak lubricin immunolabeling of chondrocytes; magnification x20; scale bar: 100 µm. E) No immunoreaction was observed in the negative control treated with PBS without the primary antibodies (tissue explanted); magnification x20; scale bar: 100 µm. F) Percentage of lubricin positive cells out of the total number of cells counted in control cartilage and in OA cartilage.
Statistical analysis

All variables were normally distributed. Comparisons between two means were tested with the Student’s t-test; comparisons between different means were tested with ANOVA test. P-values of less than 0.01 were considered statistically significant. Ten fields from randomly selected slides were observed under fluorescence and a light microscope. Each field was photographed with a digital camera. On each photomicrograph three observers, blinded to the type of sample, identified and counted the number of total cells as well as the number of these cells exhibiting a positive reaction. The proportion of positive cells was calculated for each photomicrograph and a mean value was obtained for each sample. The results were expressed as a percentage. All data were analyzed with the SPSS program (SPSS® release 16.0, Chicago, IL, USA).

Cohen’s kappa was applied to measure the agreement between the three observers and averaged over all three to evaluate overall agreement using the following grading: 0-0.2 (slight), 0.21-0.40 (fair), 0.41-0.60 (moderate), 0.61-0.80 (substantial), and 0.81-1.0 (almost perfect).

Results

Immunohistochemistry

Lubricin immunohistochemical staining in explanted tissue was appreciated in an overall extracellular matrix (ECM) of cells of both normal and OA specimens. Articular cartilage displayed a layer of lubricin on the surface of tissues. However different patterns of immunopositive cells in the two sets of specimens were appreciated. Expression of lubricin was investigated via immunohistochemistry, in vivo explanted tissue. A very strong lubricin staining (IS, 4; ES, ++++) was observed in control cartilage where almost all chondrocytes were immunolabeled (Figure 1A,B,C). On the other hand a weak lubricin immunoreaction (IS, 1; ES, +) was appreciated in OA cartilage where few cells were immunostained (Figure 1D). No immunoreaction was observed in the negative control treated with PBS without the primary antibodies (Figure 1E). Both ES and IS were significantly greater (P<0.01) in control cartilage compared to OA cartilage. Interobserver agreement, measured using the Kappa coefficient, was 0.94 (almost perfect).

In PEGDA hydrogel light microscopy observation showed different patterns of immunopositive cells in the two sets of specimens. Expression of lubricin was investigated via immunohistochemistry, in control chondrocytes and in OA chondrocytes encapsulated in
PEGDA hydrogel at 3, 4 and 5 weeks of culture. A strong (IS, 3; ES, ++++) lubricin immunoreaction was shown in control chondrocytes after 3 weeks of culture and many chondrocytes were immunolabeled (Figure 2A). After 4 weeks of culture the immunoreactions was strong (IS, 3; ES, ++++) (Figure 2B) and after 5 weeks of culture was very strong (Figure 2C) (IS, 4; ES, ++++) were almost all the chondrocytes were immunolabeled by lubricin suggesting an increased expression. No immunoreaction was observed in the negative control (IS, 0; ES, 0) (Figure 2D). A weak/moderate (IS, 1; ES, ++) lubricin immunoreaction was seen in OA chondrocytes encapsulated in PEGDA hydrogels after the 3rd week of culture and nearly half chondrocytes were immunostained (Figure 3A, B). After 4 weeks of culture strong (IS, 3; ES, ++++) lubricin immunoreaction was demonstrated in OA chondrocytes encapsulated in PEGDA hydrogels (Figure 3C) and after 5 weeks of culture was very strong compared with control chondrocytes (IS, 4; ES, ++++) (Figure 3D). IS and ES were significantly greater (P<0.01) in control chondrocytes compared with OA chondrocytes, at the 3rd, 4th and 5th weeks (Figure 4). Interobserver agreement, measured using the Kappa coefficient, was 0.91 (almost perfect).

Immunocytochemistry

Fluorescence microscopy observation showed a detection of lubricin in cells from control cartilage and in OA cartilage after the 4 passages using immunocytochemistry. Strong (IS, 4; ES, ++++) lubricin immunoreaction was observed in control cartilage (Figure 5A). The chondrocytes from OA cartilage exhibited a weak (IS, 1; ES, +) lubricin immunoreaction, with only few cells fluorescing (Figure 5B). No immunoreaction was observed in the negative control treated with 1% BSA without the primary antibodies (Figure 5C). ES was significantly greater (P<0.01) in control chondrocytes compared to OA chondrocytes (Figure 5D). Interobserver agreement, measured using the Kappa coefficient, was 0.91 (almost perfect).

Western blot

In this study, we also examined, by Western blot, the production of lubricin in human monolayer chondrocytes from normal and OA cartilage. On the 24th day we have investigated the effects of different cultures on the release of lubricin. Negligible amounts of lubricin were produced by monolayer chondrocytes from OA cartilage. In contrast, lubricin potentially was induced by chondrocytes from normal cartilage (Figure 6).

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Figure 4. Percentage of lubricin positive cells out of the total number of cells counted in control chondrocytes and in OA chondrocytes after 3, 4 and 5 weeks in PEGDA hydrogels.

Figure 5. A) Lubricin immunocytochemistry (cytoplasmic and perinuclear immunolabeling) specimen from control chondrocytes; strong lubricin immunolabeling in cells at fourth passage of culture; magnification x20; scale bars: 100 µm. B) Lubricin immunocytochemistry (cytoplasmic and perinuclear immunolabeling) specimen from OA chondrocytes; weak lubricin immunolabeling in cells at fourth passage of culture; magnification x20; scale bar: 50 µm. C) No immunoreaction was observed in the negative control treated with PBS without the primary antibodies; magnification x20; scale bar: 100 µm. D) Percentage of lubricin positive cells out of the total number of cells counted in control chondrocytes and in OA chondrocytes.

Figure 6. Lubricin expression induced in human monolayer chondrocytes from normal cartilage and human monolayer chondrocytes from OA cartilage determined by Western blot analysis. Data show the relative expression (mean ± SEM) of lubricin calculated as arbitrary densitometric units (A.D.U.) collected from three independent experiments. *P<0.01 compared to monolayer chondrocytes.
Discussion

New therapeutic strategies for OA cartilage deterioration are a novel biomedical challenge. As we know, tissue engineering focuses on restoration, maintenance, or improvement of tissue function through the development of biological substitutes. The principle obstacle for clinical transplantation today is the shortage of donor organs. For this reason, tissue engineering and regenerative medicine have become promising and important fields of research that may offer new sources of tissues and organs for transplantation. Poly (ethylene glycol) (PEG) based hydrogels have attracted wide interest as a scaffolding material for tissue engineering applications.29-32 Hydrogels encompass a class of scaffolds with many attractive features for cartilage tissue engineering.29-32 Hydrogels are made from water-soluble polymer chains that are cross-linked to form water-insoluble gel networks. Cells in the polymer solution can be encapsulated into the hydrogel during the cross-linking process. The resulting gel network can be designed to have a high water content, enabling efficient transport of nutrient and waste products to and from cells. Polymer cross-linking and hydrogel formation can be achieved by various physical and chemical mechanisms.31 This scaffold, like some others, is thus designed to perform a number of biological functions including stimulation of cells to synthesize ECM, proliferate, migrate, prevent apoptosis, and/or differentiate. The characterization of extracellular matrix anabolic factors and proteins produced by cells in the scaffolds is critical to evaluate the success of a tissue engineering system.

In this study we have evaluated lubricin expression in chondrocytes from articular cartilage of the knee, from patients with OA and compared them to normal cartilage chondrocytes, both in vivo, on paraffin sections, this evaluation was also carried out after chondrocytes encapsulation in hydrogel PEGDA, in vitro after isolation of these chondrocytes and through western blot analysis.

Lubricin is a chondroprotective glycoprotein, which acts as a vital counteragent against aberrant protein and/or cellular adhesion, infiltration and over-proliferation, and serves as a critical boundary lubricant between opposing cartilage surfaces. This protein is less expressed with aging and during OA, moreover the lubricin gene is differently expressed in the synovium of RA and OA implying a possible role in the pathogenesis of these diseases.24 Furthermore, impaired lubricin expression is associated with the onset of early OA in a sheep meniscectomy model.35

Here, for the first time, we have shown that lubricin is down regulated in OA cartilage explants and cell cultures from knee joints. This result is in line with previous studies that advocate intraarticular supplementation with lubricin for OA joints.26-27 More interestingly, we demonstrated in our study that OA chondrocytes encapsulated in PEGDA scaffolding are able to restore lubricin biosynthesis. In fact, after 4 weeks of culture of OA chondrocytes encapsulated in PEGDA hydrogel, lubricin expression nearly reached the level of the control scaffold. This increased expression of lubricin in OA chondrocytes may, somehow, be related to the absence of cytokines, which seem to influence lubricin biosynthesis. A disregulation of lubricin metabolism, under the influence of elevated cytokine concentrations in diseased or damaged joints, has been described14,35,36 and this, in time, might thereby lead to lubrication deficiencies and loss of function. In this respect, it has been claimed that a decrease in synovial fluid lubricin concentrations following anterior cruciate ligament injury may place the joint at an increased risk of wear-induced damage, as a consequence of lack of boundary lubrication, potentially leading to secondary osteoarthritis.

In this study, we clearly demonstrated that OA chondrocytes grown in PEGDA hydrogels were able to express lubricin. This investigation shows an increased expression of lubricin in chondrocytes encapsulated in hydrogel PEGDA scaffolding from OA patients after 3, 4 and 5 weeks of culture. In particular, chondrocytes from OA cartilage after 5 weeks of culture in hydrogels (PEGDA) showed an increased expression of lubricin comparable to the control cartilage. These are preliminary data, and further studies using a longer incubation time will be useful to better understand the potential effect of PEGDA. In conclusion our study suggests the possibility of applying autologous cell transplantation (ACT) in conjunction with scaffolding materials for repairing cartilage lesions in patients with OA in order to reduce, at least, the progression of the disease.

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