Probing the salt dependence of the torsional stiffness of DNA by multiplexed magnetic torque tweezers

Franziska Kriegel1, Niklas Ermann1, Ruaridh Forbes2, David Dulin2,3, Nynke H. Dekker2 and Jan Lipfert1,*

1Department of Physics, Nanosystems Initiative Munich, and Center for Nanoscience, LMU Munich, Amalienstrasse 54, 80799 Munich, Germany, 2Department of Bionanoscience, Kavli Institute of Nanoscience, Delft University of Technology, Van der Maasweg 9, 2629 HZ Delft, The Netherlands and 3Junior Research Group 2, Interdisciplinary Center for Clinical Research, Friedrich-Alexander-University Erlangen-Nürnberg (FAU), Hartmannstrasse 14, 91052 Erlangen, Germany

Received February 27, 2017; Revised April 04, 2017; Editorial Decision April 05, 2017; Accepted April 28, 2017

ABSTRACT

The mechanical properties of DNA fundamentally constrain and enable the storage and transmission of genetic information and its use in DNA nanotechnology. Many properties of DNA depend on the ionic environment due to its highly charged backbone. In particular, both theoretical analyses and direct single-molecule experiments have shown its bending stiffness to depend on salt concentration. In contrast, the salt-dependence of the twist stiffness of DNA is much less explored. Here, we employ optimized multiplexed magnetic torque tweezers to study the torsional stiffness of DNA under varying salt conditions as a function of stretching force. At low forces (<3 pN), the effective torsional stiffness is ∼10% smaller for high salt conditions (500 mM NaCl or 10 mM MgCl2) compared to lower salt concentrations (20 mM NaCl and 100 mM NaCl). These differences, however, can be accounted for by taking into account the known salt dependence of the bending stiffness. In addition, the measured high-force (6.5 pN) torsional stiffness values of C = 103 ± 4 nm are identical, within experimental errors, for all tested salt concentrations, suggesting that the intrinsic torsional stiffness of DNA does not depend on salt.

INTRODUCTION

DNA is the carrier of genetic information in all cellular life. In addition to its sequence, its polymeric and mechanical properties are critical for its biological function. For example, in our cells ∼2 m of DNA are packed into ∼10 μm-sized nucleus (1), involving a multitude of deformations and DNA–protein interactions. In vivo DNA is negatively supercoiled and both supercoiling and DNA packing play important roles in gene regulation (2–7). In addition to its biological role, DNA is emerging as a building block for artificially created 3D nanostructures (8). A detailed and quantitative description of DNA mechanical properties is a prerequisite to understanding its biological roles and for its optimal use as a construction material at the nanoscale.

At length scales significantly longer than 1 bp, DNA is commonly modeled as an isotropic elastic rod, with a bending persistence length A, stretch or Young’s modulus B, torsional stiffness C and twist-stretch coupling D (9,10). All four elastic constants have been determined for DNA in vitro in a series of ingenious single-molecule manipulation measurements (11–20). However, their values, in general, can depend on solution conditions. In particular, salt concentration can strongly modulate DNA properties, as DNA is highly negatively charged (21). In a classic argument, Odijk (22) and independently Skolnick and Fixman (23) derived how electrostatic repulsion increases DNA bending stiffness, A, and how the bending persistence length can be separated into a salt-independent and a salt-dependent contribution. Subsequently, single-molecule stretching experiments have determined the salt dependence of A for DNA (24,25) and recently also for RNA (26,27) and indeed found a reduction of A by ∼20% going from low (<20 mM monovalent salt) to relatively high (>300 mM monovalent or ∼10 mM divalent salt) ionic strength. However, the exact nature and molecular details of this dependence remain an area of active research (28–38).

The essence of the Odijk and Skolnick-Fixman argument is that bending a charged rod will bring charges into closer proximity, which will cost more energy if there are fewer screening counterions and, therefore, the stiffness will be in-

*To whom correspondence should be addressed. Tel: +49 89 2180 2005; Fax: +49 89 2180 2050; Email: Jan.Lipfert@lmu.de

Present addresses:
Niklas Ermann, Cavendish Laboratory, University of Cambridge, Cambridge CB3 0HE, UK.
Ruaridh Forbes, Department of Physics and Astronomy, University College London, Gower Street, London WC1E 6BT, UK.

© The Author(s) 2017. Published by Oxford University Press on behalf of Nucleic Acids Research. This is an Open Access article distributed under the terms of the Creative Commons Attribution License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted reuse, distribution, and reproduction in any medium, provided the original work is properly cited.
creased at low salt. In contrast, for a homogenously charged rod, twisting the rod does not alter the distance between charges, which would suggest the twist-stiffness not to depend on salt. For real molecules the charges are localized, though; in DNA, the phosphate groups carry the negative charges under physiological conditions and it is not \textit{a priori} clear whether the torsional stiffness would depend on salt.

Several properties of DNA under torsional constraint, in particular aspects of DNA supercoiling, are known to strongly depend on salt concentration (39–42). Under sufficient torsional stress, DNA undergoes a buckling transition and forms plectonemic supercoils. Due to electrostatic repulsion, the diameter of plectonemic supercoils increases with decreasing salt concentrations (43–46). In addition, the critical linking number for buckling (19,47), the number of plectonemes (48,49), as well as their dynamics (42) have all been found to depend on salt concentration. However, plectonemic supercoils involve strong bending and bring DNA segments into close proximity and these observations, therefore, do not directly probe the torsional stiffness in isolation. Neukirch suggested from theoretical analysis of magnetic tweezers (MT) measurements on supercoiled DNA that the torsional stiffness of DNA decreases almost 2-fold upon addition of millimolar concentrations of Mg$^{2+}$ ions (43). Similarly, direct torque measurements using a rotor bead assay suggested a small decrease of the torsional stiffness with increasing ionic strength (~10%) in going from buffer only to ~150 mM monovalent salt and no additional decrease, within experimental error, upon further addition of ~1.8 M monovalent salt; at 10 pN stretching force (50). In contrast, Delrow \textit{et al.} found an increase in torsional stiffness in fluorescence polarisation anisotropy (FPA) measurements by ~20% upon addition of 5 mM Mg$^{2+}$ (51). Finally, indirect torque measurements by thermodynamic integration (19) and Monte Carlo modeling (45) of MT measurements on supercoiled DNA concluded the torque at and past the buckling transition to depend on salt, but suggested little dependence of the torsional stiffness on ionic strength. In summary, the dependence of the torsional stiffness of DNA on salt concentration and valence is currently debated, in particular due to the lack of systematic and direct measurements.

Here, we demonstrate multiplexed magnetic torque tweezers (mMTT) that enable parallelized single-molecule torque measurements. Using this experimental approach, we determine the torsional stiffness of DNA as a function of applied stretching force and salt concentration. Our mMTT instrument is an extension of conventional MT that have proven to be a powerful tool to investigate the torsional properties of nucleic acids (10,52,53). In MT and mMTT, molecules of interest are tethered between a flow cell surface and magnetic particles (Figure 1). Bead positions are tracked by video microscopy, which enables tracking of many beads in parallel (54–56). Stretching forces are exerted by applying external magnetic fields that pull the magnetic particles upward. The forces can be calculated from the magnetic field gradients by taking into account the induced magnetization on the beads (57) and experimentally determined from analysis of the transverse fluctuations (52,58–61). Conventional MT can apply torque by rotating the external magnetic field, which in turn rotates the beads, however, they do not measure torque. Torque measurements on individual DNA molecules in the MT have been achieved using an indirect approach by thermodynamic integration (19) and directly by tracking the rotation angle, either of a rotor bead (15,17,50,62) or of the magnetic bead or assembly (18,20,63–65). Our mMTT implementation employs an optimized angle tracking protocol and magnet geometry to extend the multiplexing capabilities inherent in MT measurement to the torque dimension.

\section*{MATERIALS AND METHODS}

\subsection*{Magnetic tweezers instrument}

Measurements were performed with a home-built MT setup. In brief, a light emitting diode (Osram Oslon SSL, red, 165 lm) is used to illuminate the sample, monochromatically from above. An oil immersion objective (60× Plan Fluorite with correction collar, NA 0.9 or 40× Plan Fluorite, NA 0.75, Olympus) is placed on a piezo (Pifoc, P-726.1CD and controller, E-753.1CD, Physik Instrumente) stage underneath the flow cell holder. The flow cell is imaged with a mirror (20D20ER.1, Newport) and tube lens (G322304000, Newport) onto the chip of a camera (Falcon PT-41-4M60, Dalsa). Magnets (see below) are placed on a motorized arm, using a translational motor (C-863.11-Mercury controller and M-126.PD2 motor, Physik Instrumente) and a rotational motor (C-863.11-Mercury controller and C-150.PD motor, Physik Instrumente) to control the magnets’ rotation and position in Z. The flow cell outlet is connected to a pump (ISM832C, Ismatec) for fluid handling (66). The setup is controlled using a computer (DELL Precision T3600) equipped with a framegrabber (PCIe-1433, National Instruments) and using software written in LabVIEW (National Instruments) described by Cnossen \textit{et al.} (56).

\subsection*{DNA construct and beads for MT measurements}

Measurements used a 7.9-kbp DNA construct as previously described (20). Specific and torsionally constrained coupling of the DNA to magnetic beads (streptavidin-coated 1.0 μm diameter MyOne or 2.8 μm diameter M270 beads; Life Technologies) and the flow cell surface was achieved through ligation with ~600-bp polymerase chain reaction-generated DNA fragments, comprising multiple biotin- and digoxigenin-modified dUTP moieties (Jena Bioscience, respectively). The DNA construct was first coupled to the streptavidin-coated beads by incubating 5 ng of the DNA construct with 2 μl of MyOne (or 5 μl M270) beads in a final volume of 20 μl of phosphate buffered saline (PBS; Sigma-Aldrich) for 12 min (5 min for M270 beads). The DNA-bead solution was subsequently diluted into 100 μl PBS and introduced into the flow cell.

\subsection*{Preparation of the flow cell}

Flow cells were constructed by assembly of two glass coverslips (24 × 60 mm, Carl Roth) separated by a single parafilm (PARAFILM M, H666.1, Carl Roth) layer that formed a flow channel used as the measurement chamber. The bottom coverslip was first modified using
(3-Glycidoxypropyl)trimethoxysilane (abcr GmbH), subsequently reacted for one hour with anti-digoxigenin (100 μg/ml in 1× PBS; Roche) and then passivated using a commercial passivation mix (BlockAid™ Blocking Solution, Thermoscientific) for 1 h. After excessive flushing of the flow cell using PBS buffer, the DNA-bead solution is introduced and allowed to bind for ten minutes (MyOne beads) or 50 s (M270 beads). Unbound beads are removed from the flow cell by flushing with ~500 μl PBS.

**Bead selection**

To verify that selected beads are bound to a single, torsionally constrained DNA tether, several tests were performed using conventional MT that employed a pair of cubic permanent magnets (5 × 5 × 5 mm³; W-05-N50-G, Supermagne, Switzerland), oriented in a vertical configuration (57) with a spacing of 1 mm. First, the external magnets are moved vertically to exert alternating forces of ~5 pN (to fully stretch the molecule) and ~0.01 pN (close to zero force) in order to test the contour length of the tethers. The measured change in extension is expected to be approximately the contour length of the DNA double-strand. Next, magnets are rotated clockwise by 20 turns at high (5 pN) tension to test for multiple tethers: At forces >1 pN, DNA does not form plectonemic supercoils upon unwinding (corresponding to counterclockwise rotation), but melts instead (67) and no decrease in the extension is expected for single DNA tethers (Figure 2B). In contrast, if a bead is attached via two or more double-stranded DNA molecules, the molecules will form braids if the bead is rotated, causing a decrease in the molecule’s extension, independent of stretching force. To select for beads that are courable (i.e. with a fully double-stranded backbone and attached via multiple attachment points at both ends) magnets are rotated by 20 turns in both directions at 0.6 pN to check for DNA supercoiling (Figure 2A), which is seen in a decrease in the detected extension. Finally, the flow cell was flushed with ~500 μl of the appropriate measurement buffer, see Table 1.

**Magnetic torque tweezers configuration and measurement protocol**

Conventional MT do not allow direct measurements of torque (20); for single-molecule torque measurements the cubical magnets are, therefore, replaced by a set of cylindrical magnets (Figure 1A) that are assembled as a stack of three ring magnets with an outer diameter of 6 mm, a 2 mm diameter aperture in the center and a height of 2 mm per magnet (R-06-02-02-G, Supermagne, Switzerland). A cylindrical magnet with 3 mm diameter and 6 mm height (S-03-06-N, Supermagne, Switzerland) is used as a ‘side magnet’. This magnet configuration exerts an upward pulling force (20,60) while providing a weak rotational trap suitable for torque measurements. Details and optimization of the magnet configurations are further discussed below. Between rotating the magnets, we measured the angle fluctuations at a fixed number of applied turns for 100–200 s for MyOne and M270 beads. The characteristic time scales of rotational fluctuations are ~0.1 and ~0.5 s for MyOne and M270 beads, respectively, in MTT representative for our conditions (20,64,65). Our measurement intervals, therefore, correspond to >100 times the characteristic time scale of angular fluctuations. We note that our camera integration time of ~17 ms (corresponding to the frame rate of 60 Hz) is significantly shorter than the characteristic time scale of rotational fluctuations, making blurring and aliasing effects negligible (59,68). The rotation speed of the magnets for under- and overwinding of the DNA tethers by integer number of turns during torque measurements was set to 0.1 Hz.

**Data averaging of multiple single-molecule measurements**

Torque measurements on dsDNA were performed for a range of forces and salt conditions (see ‘Results’ section and Figures 2 and 3). In order to improve the signal-to-noise ratio in the torque and extension versus turns measurements, data for several independent DNA tethers were averaged for each condition. First, the responses of multiple DNA molecules to an applied number of turns were collected and analyzed; subsequently, the curves were aligned to yield single, averaged extension-rotation and torque-rotation curves for each force and salt condition. For measurements at forces of <1 pN, the rotation-extension curves are symmetric about zero turns (Figure 2A). For alignment, a Gaussian was fitted to the individual extension-rotation curves of independent DNA molecules (Figure 2C). The position of the maximum determined from the fit was defined as $L_{\Delta 0}$, the number of turns at which the molecule is torsionally relaxed. The extension-rotation and torque-rotation curves were shifted along the turns-axis by $-L_{\Delta 0}$ to center the curves before averaging. For the averaging of the extension curves at forces >1 pN, a line was fitted to the constant region at negative turn values (Figure 2C). The first experimental value that fell below this line within experimental error was determined as the buckling point. Each curve was shifted along the turns-axis to align with the mean value of the buckling point of all measured DNA molecules for a given force and salt condition. Similarly, variations in the absolute extension of the molecule at zero turns were adjusted by shifting the curves. Finally, all curves for a given force and salt condition were averaged. For forces <1 pN, the data where binned in bins of two turns prior to computing the standard deviation (STD) and standard error of the mean (SEM) for both torque and extension as a function of applied turns (Supplementary Figure S13). For forces >1 pN, data were directly averaged (Supplementary Figure S14). Data points for each force and salt condition consist of at least 10 (and up to 45) independently measured molecules from at least two independent measurement runs, corresponding to an overall number of 475 measured molecules in this work. We note that the molecule-to-molecule variability (as measured by their standard deviation) of torsional measurements, in particular of the torsional stiffness, is about 10–20% in our current protocol, comparable with other single-molecule torque measurements (19,20,50). This means that averaging over multiple (≥10) independent molecules is required to reduce the standard error of the mean sufficiently to be able to probe or detect small changes. In the current study, we have system-
Table 1. Buffer conditions and salt concentrations

| Salt   | Tris  | EDTA | NaCl | MgCl₂ |
|--------|-------|------|------|-------|
| 1      | 10 mM | 1 mM | 20 mM| 0     |
| 2      | 10 mM | 1 mM | 100 mM| 0     |
| 3      | 10 mM | 1 mM | 500 mM| 0     |
| 4      | 10 mM | 1 mM | 100 mM| 10 mM|

Measurements were performed in TE-buffer at pH 7.4. Ionic strength was varied by the addition of NaCl (salt 1, 2 and 3) or a combination of NaCl and MgCl₂ (salt 4).

forces and control of the twist of the tethered molecules. Magnetic torque tweezers enable the measurement of torque at the single-molecule level by employing a magnet configuration with a weak angular trap (Figure 1B–D; see also below) and a tracking protocol that permits to track the rotation of the molecule around the tether axis. The basic principle of the torque measurement is as follows: tracking the rotation angle $\Theta$ initially for a torsionally relaxed molecule, the mean of the bead’s rotation angle $\Theta_0$ indicates the equilibrium position of the rotational trap and the magnitude of the fluctuations around the equilibrium position allows us to calibrate the stiffness of the angular trap ($k_{\text{ROT}}$):

$$ k_{\text{ROT}} = k_B T / \text{Var}(\Theta) = k_B T / (\text{Std}(\Theta))^2 $$

where $k_B$ is the Boltzmann constant and $T$ the absolute temperature. After over- or underwinding the molecule by $N$ turns, the restoring torque exerted by the molecular tether ($\Gamma_{\text{mol}}$) gives rise to a shift in the mean angle position to a new angular position $\Theta_N$ displaced from the initial equilibrium angle $\Theta_0$. The molecular torque can then be simply determined as the shift in mean angle multiplied by the rotational trap stiffness (Figure 1E):

$$ \Gamma_{\text{mol}} = -k_{\text{ROT}} < \Theta_N - \Theta_0 > $$

### Multiplexed magnetic torque tweezers

We have optimized our magnetic torque tweezers protocols to enable multiplexed measurements, i.e. to perform multiple single-molecule torque measurements in parallel. For parallel measurements, it is desirable to employ molecular constructs that avoid the need for multi-component assembly, such as the addition of a rotor bead to the DNA or a fiducial marker bead or rod to the main magnetic bead, to maximize the number of well-tethered and complete molecular constructs within a single field of view (FOV).

In our mMTT scheme (Figure 1A), we use simple double-stranded DNA constructs, attached with one end to the flow cell surface via multiple digoxigenin labels and to commercially available magnetic beads via multiple biotin-streptavidin linkages (see ‘Materials and Methods’ section), identical to constructs used routinely in conventional MT. We then exploit the particular geometry of bead fluctuations under a cylindrical magnet with a predominantly vertical field to track the beads’ rotation angles via their $(X,Y)$-positions.

Tracking rotation angle from $(X,Y)$-position. If the magnetic field is aligned exactly vertically (the so-called freely-orbiting MT or FOMT configuration with a single cylindrical magnet), the bead is free to rotate
about the tether axis and its thermal fluctuations trace out a doughnut shape (Figure 1B) in the \((X, Y)\)-plane (60). Importantly, this configuration allows tracking of the rotation angle by conversion of the \((X, Y)\)-position on the doughnut to polar coordinates (60). While the FOFT configuration enables observation of the unconstrained, rotational motion of the bead, it does not allow inducing twist. By adding a small magnet (or electromagnet (65)) to the cylindrical main magnet (Figure 1C), the magnetic field is slightly tilted (Figure 1D). The tilted field provides a (weak) rotational trap for the magnetic beads and their fluctuations in the \((X, Y)\)-plane no longer trace out the full circle, but an arc-like shape (Figure 1C). The beads still experience an upward pulling force in \(Z\) and the weak rotational trap enables to twist the molecule of interest by rotating the magnet assembly (20,60).

Importantly, the position in \((X, Y)\) can still be used to track the rotation angle of the bead. In practice, it is not necessary to align the magnets in FOFT configuration to fit the doughnut pattern; instead, it is sufficient to record the \((X, Y)\)-position while rotating the magnets and to fit a circle to the recorded trace in order to determine the radius of the molecule movement around its tether axis, which is in turn used to transform the recorded \((X, Y)\)-position of the bead to polar coordinates (Supplementary Figures S1 and 2).

Optimization of the setup and trap stiffness for parallel torque measurements. There are conflicting requirements on the stiffness of the rotational trap in MTT, which in turn depends strongly on the magnetic field direction and strength. Equation (2) implies that for a given molecular torque, the shift in equilibrium angle is inversely proportional to the trap stiffness. As a consequence, if the trap stiffness is too high \((\geq 1000 \text{ pN-nm/rad})\), typical torques exerted by DNA lead to very small shifts in the equilibrium angle \((<1^\circ)\) that are difficult or impossible to measure accurately (20). In contrast, if the trap stiffness is too low \((\leq 30 \text{ pN-nm/rad or } Std(\theta) > 20^\circ)\), the bead will not reliably follow the magnets’ rotation, therefore precluding systematic and controlled application of twist to the tether (Supplementary Figure S3).

For multiplexed measurements, we have to ensure that the trap stiffness is within these limits for the entire field-of-view \((400 \times 300 \mu\text{m}^2 \text{ at } 40 \times \text{magnification and } 260 \times 190 \mu\text{m}^2 \text{ at } 60 \times \text{magnification in our setup})\). In addition, it is desirable to have a homogeneous gradient of the field along the \(Z\)-direction to ensure that all tethers experience similar stretching forces. To guide and optimize the choice of magnet configuration to satisfy these requirements, we carried out simulations of the axial and radial fields for our MTT magnet configuration.

We calculated the magnetic field vectors for the magnet configurations used in FOFT (Figure 1B) and (m)MTT (Figure 1C) with the equivalent source method and exploiting the superposition principle (Supplementary Figure S4) (57,65). The cylindrical magnet with a hollow center used in FOFT is equivalent to two superimposed solid cylindrical magnets with opposite magnetization and the effect of the side magnet in the (m)MTT is added by considering an additional, laterally offset cylindrical magnet. We calibrated the remanent field of our magnets through field measurements using a Hall Probe (Supplementary Figure S5). Furthermore we tested our field calculations against Hall probe field measurements along \(Z\) and \(X\) and found excellent agreement (Supplementary Figures S6 and 7). The magnetic field configurations for both FOFT and MTT (Figure 1D and Supplementary Figure S8) have the field and field gradient predominantly in the \(Z\)-direction. Importantly, the gradient of the magnetic field, which essentially sets the force exerted on the beads, varies only by 0.5% over 400 \(\mu\text{m}\) in \(X\) (which corresponds to the largest extension of the FOV used in this work) for the MTT configuration. The essentially constant field gradient implies that all tethered beads in the FOV experience the same force, only limited by the \(\sim 10\%\) variation in total magnetization for the beads employed in this study (57,60,71).

For the FOFT configuration, the radial field (i.e. \(X\) or \(Y\)) is zero directly under the cylindrical magnet, while adding the side magnet in the (m)MTT configuration adds a field component in \(X\) (Figure 1D and Supplementary Figure S8). We found that for high-resolution torque measurement, in particular with the larger M270 beads, it is advantageous to lower the \(X\)-component of the field and, therefore, the trap stiffness. A displacement by \(\sim 400 \mu\text{m}\) reduces the trap stiffness \(\sim 3-4\text{-fold}\), to 100–300 \text{ pN-nm/rad}, compared to the alignment centered on the cylindrical magnet (Supplementary Figure S3). The rotational trap stiffness decreases with increasing distance of the magnet from the flow cell and, therefore, with decreasing force (Supplementary Figure S9). While the trap stiffnesses fall into the usable range of 30–1000 \text{ pN-nm/rad} for all studied forces, we found it advantageous for low force torque measurements to bring the magnets closer to the flow cell (to 3–4 mm), corresponding to forces of 3–6 \text{ pN}, for the segments of the torque measurement traces during which the magnets are actively rotated, to ensure that the beads reliably follow the magnets’ rotation.

For multiplexed torque measurements, it is important to not only have uniform forces across the FOV, but also uniform rotational trap stiffnesses. We found the variation in rotational trap stiffness for the same bead to only vary by \(<10\%\) at different positions across the FOV (Supplementary Figure S10). The variability across the FOV is much less than the \(\geq 20\%\) bead-to-bead variability of the rotational trap stiffness at the same position in the flow cell (Supplementary Figure S10) that appears to stem from variations in the magnetic anisotropy of the beads employed (70,72). In practice, the variability in rotational trap stiffness is not a critical limitation, though, since the values tend to fall into the workable range of trap stiffnesses and since the same angle traces recorded for torque determination (Equation 2) are also used for the trap stiffness calibration via Equation (1). In practice, after discarding beads that are attached via multiple DNA tethers, nicked molecules or which are too close to other beads (which leads to tracking errors), we can simultaneously track currently up to 40 M270 beads or 80 MyOne DNA-tethered beads.

Probing the torque response of dsDNA using mMTT

Our mMTT setup enabled us to systematically investigate the response of dsDNA under different salt conditions. We recorded the extension and the rotation angle around the tether axis, which is converted to torque via Equation (2),
torque versus turn response (Figure 2F):

$$C_{\text{eff}} = \frac{L_C}{(2\pi N k_B T)} \cdot \Gamma_{\text{mol}, N}$$

$$= \frac{L_C}{(2\pi k_B T)} \cdot \left( \Gamma_{\text{mol}, N} / N \right)$$ (3)

Here $L_C$ is the contour length of the molecule and $N$ the applied number of turns, thus $C_{\text{eff}}$ is in units of length and can be interpreted as a twist persistence length, in direct analogy to the bending persistence length $A$.

**Extension-rotation and torque-rotation responses of dsDNA in different salt concentrations.** We systematically recorded the extension and torque response of multiple DNA molecules and averaged the results for each force and salt condition (see ‘Materials and Methods’ section) including a total of 475 DNA molecules. For the measurements we chose a set of salt conditions (Table 1) that included monovalent salt concentrations from low (20 mM; ‘salt 1’) to high concentrations (500 mM; ‘salt 3’), including a point at near physiological monovalent salt concentration (100 mM; ‘salt 2’). In addition, we included measurements with 10 mM MgCl$_2$ added (‘salt 4’); Mg$^{2+}$ is the physiologically most abundant divalent ion and 10 mM Mg$^{2+}$ is a typical ‘high’ concentration, used e.g. to induce RNA folding in *in vitro* measurements (21). We note that these salt conditions cover the range typically used in *in vitro* studies of for e.g. RNA folding, nucleic acid–protein interactions or nucleic acid nanotechnology.

Averaged high-resolution extension-rotation and torque-rotation data from mMMT measurements resolve a salt dependence of dsDNA when applying turns (Figure 3). The response in extension (Figure 3A–C) and torque (Figure 3D–F) are similar for salt 1 and 2 and for salt 3 and 4. For further discussion we averaged the low salt conditions (salt 1 and 2, blue colors) and independently averaged the high salt conditions (salt 3 and 4, green colors).

A large difference is observed between salt 1 and the higher salt conditions at 0.9 pN: While the extension-rotation curves are symmetric for the high salt conditions at this force, the response for salt 1 is asymmetric, indicating DNA melting upon underwinding. The lower salt concentration leads to a relative destabilization of the DNA double helix and thus to an earlier onset of DNA melting, consistent with previous reports (67,75).

**Buckling points.** The buckling points correspond to the number of turns at which the DNA molecule starts to form plectonemes when being over- or underwound. Here we report the buckling points in units of the supercoiling density (Figure 3G), which is the change in linking number (i.e. the applied number of turns) normalized to the number of turns in the torsionally relaxed helix, 1 turn per 10.5 bp. The transition from an overwound (or underwound for forces smaller 1 pN) to a straight molecule (pre-buckling) to a buckled molecule depends on the ionic surrounding.

The effective torsional stiffness of DNA can be determined from the experimentally measured torque versus turns response, by fitting a slope to the linear region of the

![Figure 2](https://academic.oup.com/nar/article-abstract/45/10/5920/3782594/56x585-303x722)
undergoing the buckling transition. We observe the force-dependence of the buckling torques to follow the empirical power law proposed by Mosconi et al. (19) (Supplementary Figure S16B).

The observed buckling torques are in good agreement with the mechanical model by Marko (76) (Figure S1). To fit the buckling points, slopes in the plectonemic regime and buckling torques in the framework of the Marko model, we used a fixed value for the intrinsic torsional stiffness \( C = 110 \text{nm} \) and the known values \( A = 48 \text{ and } 43 \text{ nm} \) for the bending persistence length at low and high salt, respectively. Our choice of \( C \), notably taken to be independent of salt concentration, is a consensus value from previous studies (15,20,77) for the intrinsic torsional stiffness of DNA, corresponding to the high-force limit (see below). The values for the bending stiffness \( A \) under low and high salt conditions are typical average values for the corresponding salt conditions obtained in a number of different single-molecule studies (12,25–27,78) (see Supplementary Figure S1k of Ref. (27) for an overview). The stiffness of the plectonemic state \( P \) at low salt and high salt was first fitted individually to the buckling points, slopes in the plectonemic regime and the buckling torque data. We then averaged the resulting values for \( P \) and found \( P = 20 \pm 4 \text{ nm} \) and \( P = 15 \pm 4 \text{ nm} \) for low salt and high salt, respectively. We note that our value of \( 20 \pm 4 \text{ nm} \) at low salt is in agreement with the range of \( 21–27 \text{ nm} \) suggested for these salt conditions; in addition, the observed decrease of \( P \) at high salt is as predicted by Marko (76).

In summary, our data on the behavior of DNA post-buckling is in agreement with previous results (19,41,45) and the effect of salt on DNA at the buckling point and in the post-buckling regime is at least semi-quantitatively described by the twistable worm-like chain model taking into account the known change in the bending persistence length and adjusting the torsional stiffness of the plectonemic state \( P \). We find \( P \) to be \( 30\% \) larger under our low salt conditions compared to high salt, which likely reflects the fact that in the plectonemes the DNA is sharply bent and segments of DNA are brought into close proximity.

**Post-buckling extension-rotation slopes.** As negatively charged segments of DNA are brought into proximity in plectonemes, the radius (the size) of the plectonemes is strongly dependent on electrostatic interactions (41,45). For low salt conditions overall ionic screening is small, therefore electrostatic repulsion in the plectoneme is larger compared to the higher salt buffers, giving rise to a larger plectoneme radius and larger magnitude of the post-buckling slope at lower salt (Figure 3H), in agreement with previous measurements (19). The force-dependence of the post-buckling slope follows an empirical power law behavior, in quantitative agreement with the results of Mosconi et al. (19) (Supplementary Figure S16A). In addition, the force and salt dependence of the slope in the plectonemic region are again reasonably well described by the mechanical model for DNA (Figure 3H), as discussed in the next subsection.

**Buckling torque.** The measured molecular torque of ds-DNA increases linearly up to the buckling transition for positive turns (41,45). We use the mean of the values in the plateau in the post-buckling regime to compute the buckling torque. Buckling torque increases with increasing force (see also Figure 2). The observed values are slightly lower for high salt compared to low salt (Figure 3I). Due to electrostatic repulsion at low ionic strength, dsDNA is able to store more molecular torque compared to high salt before

**Figure 3.** Averaged extension-rotation and torque-rotation responses of dsDNA for different salt conditions. Averaged extension versus turns data for four different buffers and corresponding averaged torque versus turns data at 0.4 pN (A and D), 0.9 pN (B and E) and 2 pN (C and F). Blue colors indicate measurements at low salt (salt 1 and 2); green colors indicate measurements at high salt (salt 3 and 4; see Table 1 for salt conditions). (G) (Normalized) buckling points as a function of force. We averaged salt 1 and 2 to low salt (blue) and salt 3 and 4 to high salt (green). (H) Post-buckling slopes, determined from the averaged extension-rotation data against force. Same color code as in G. (I) Buckling torque derived from the torque versus turn data. Color code as in G. Indicated with a filled, square symbol is the measured transition from B-DNA to P-DNA at 6.5 pN. Co-plotted in panels G–I is the Marko model (dashed lines) for dsDNA with fixed parameters: \( C = 110 \text{nm} \), \( A = 43 \text{ nm} \) for high salt conditions and \( 48 \text{ nm} \) for low salt conditions) and \( P_{\text{low}} = 20 \text{ nm} \) or \( P_{\text{high}} = 15 \text{ nm} \).  

\[ \text{Post-buckling extension-rotation slopes.} \] As negatively charged segments of DNA are brought into proximity in plectonemes, the radius (the size) of the plectonemes is strongly dependent on electrostatic interactions (41,45). For low salt conditions overall ionic screening is small, therefore electrostatic repulsion in the plectoneme is larger compared to the higher salt buffers, giving rise to a larger plectoneme radius and larger magnitude of the post-buckling slope at lower salt (Figure 3H), in agreement with previous measurements (19). The force-dependence of the post-buckling slope follows an empirical power law behavior, in quantitative agreement with the results of Mosconi et al. (19) (Supplementary Figure S16A). In addition, the force and salt dependence of the slope in the plectonemic region are again reasonably well described by the mechanical model for DNA (Figure 3H), as discussed in the next subsection.

**Buckling torque.** The measured molecular torque of ds-DNA increases linearly up to the buckling transition for positive turns (41,45). We use the mean of the values in the plateau in the post-buckling regime to compute the buckling torque. Buckling torque increases with increasing force (see also Figure 2). The observed values are slightly lower for high salt compared to low salt (Figure 3I). Due to electrostatic repulsion at low ionic strength, dsDNA is able to store more molecular torque compared to high salt before

**Figure 3.** Averaged extension-rotation and torque-rotation responses of dsDNA for different salt conditions. Averaged extension versus turns data for four different buffers and corresponding averaged torque versus turns data at 0.4 pN (A and D), 0.9 pN (B and E) and 2 pN (C and F). Blue colors indicate measurements at low salt (salt 1 and 2); green colors indicate measurements at high salt (salt 3 and 4; see Table 1 for salt conditions). (G) (Normalized) buckling points as a function of force. We averaged salt 1 and 2 to low salt (blue) and salt 3 and 4 to high salt (green). (H) Post-buckling slopes, determined from the averaged extension-rotation data against force. Same color code as in G. (I) Buckling torque derived from the torque versus turn data. Color code as in G. Indicated with a filled, square symbol is the measured transition from B-DNA to P-DNA at 6.5 pN. Co-plotted in panels G–I is the Marko model (dashed lines) for dsDNA with fixed parameters: \( C = 110 \text{nm} \), \( A = 43 \text{ nm} \) for high salt conditions and \( 48 \text{ nm} \) for low salt conditions) and \( P_{\text{low}} = 20 \text{ nm} \) or \( P_{\text{high}} = 15 \text{ nm} \).
Figure 4. The effective twist persistence length of dsDNA for different salt conditions. The effective twist persistence length $C_{\text{eff}}$ as a function of force and salt. Data points are the means and standard errors of the mean from 10-45 independent molecules for each salt and force condition. (A) $C_{\text{eff}}$ increases strongly with force, saturating for high forces at ~100 nm for all salts. See Table 1 for salt conditions. (B) $C_{\text{eff}}$ for all four salt conditions at 0.4 pN and 6.5 pN. Color code as in A. (C) low salt (salt 1 and 2, blue) versus high salt (salt 3 and 4, green) torsional stiffness data (see main text) show a trend to be slightly lower for higher salt concentrations. The MN model is co-plotted (solid line), with fixed values $C = 110$ nm and $A = 48$ nm (low salt, blue) and $A = 43$ nm (high salt, green). (D) The ratio of the low salt $C_{\text{eff}}$ data and the high salt $C_{\text{eff}}$ as a function of force. Two models, the MN model (black line) and the aTWLC model (black squares) are co-plotted with the experimental data (red circles).

pN), the measured torsional stiffness values converge and at 6.5 pN $C_{\text{eff}}$ is identical, within experimental errors, for all salt concentrations (Figure 4A and B). However, for lower forces ($F < 3.5$ pN) small but systematic differences between the different salt concentrations are apparent: the lower salt concentrations tend to give rise to higher $C_{\text{eff}}$ values in the low force regime (Figure 4A and B). Running an n-way ANOVA on the $C_{\text{eff}}$ values with salt and force as factors, we find that $C_{\text{eff}}$ varies statistically significantly with force ($P = 1.3 \times 10^{-54}$) and salt ($P = 0.046$). For clarity, we again averaged the two low salt concentrations and the two high salt concentrations; the resulting averaged values show the trend even more clearly (Figure 4C): An n-way ANOVA with salt and force as factors finds $P = 0.0069$ for the dependence on salt and $P = 6.6 \times 10^{-37}$ for the dependence on force. We note that the same trends are observed when measuring individual molecules under the different conditions (see e.g. Supplementary Figure S12); however, given the measurement uncertainty of ~10–20% standard deviation, we focused on the averaged values for each condition to draw statistical significant conclusions.

The effective torsional stiffness is independent of salt concentration at high forces ($F > 6$ pN), but systematically and statistically significantly lower for high salt in particular in the intermediate force regime (0.9–2.0 pN) (Figure 4C). The fact that the effective torsional stiffness deviates from the ‘true’ intrinsic torsional stiffness value and decreases with decreasing force has been investigated before and can be (at least qualitatively) understood by taking into account the coupling between bending and twisting fluctuations, in particular using the perturbative model by Moroz and Nelson (MN). Taking into account the known dependence of the bending persistence length on salt (and assuming a salt-independent value for the intrinsic torsional stiffness), the MN model predicts relative differences between the high and low salt conditions that are in good agreement, within experimental errors, with our measurements (Figure 4D, solid black line; reduced $\chi^2 = 1.0$). In contrast, the data are less consistent with the ratio of $C_{\text{eff}}$ at low versus high salt being equal to one (Figure 4D, dashed horizontal line; reduced $\chi^2 = 1.92$).

Unfortunately, the MN model does not quantitatively account for the force dependence of $C_{\text{eff}}$ and overestimates $C_{\text{eff}}$ at intermediate and low forces (0.2–2 pN) (Figure 4C). This shortcoming of MN theory has been described and investigated in a number of recent publications. Extensions of the MN model have been proposed, to account for the systematic deviations between the MN model and experimental data (80). One particular extension of MN is to extend the underlying isotropic rod model to include an anisotropy, i.e. distinguish between bending deformations between the two orthogonal directions that are perpendicular to the helix axis. First introduced by Marko and Siggia (81), this anisotropic rod model (aTWLC) has recently been investigated by Nomidis et al. by extensive coarse grained computer simulations (Nomidis, S., Kriegel, F., Vanderlinden, W., et al.; in preparation); the results suggest that introducing a non-zero twist-bend coupling constant (which is zero by definition in the isotropic rod model) can quantitatively account for the previously published $C_{\text{eff}}$ versus $F$ data. Unfortunately, our current implementation of the coarse-grained model does not explicitly account for electrostatics. However, again taking into account only the changes in bending persistence length with salt and keeping the intrinsic torsional stiffness fixed, the aTWLC model predicts differences of the high and low salt values for $C_{\text{eff}}$ very similar to the MN model and consistent with experimental data (Figure 4D, black squares; reduced $\chi^2 = 1.15$).

CONCLUSION

We have developed and optimized an mMTT setup that enables parallel measurements of torque at the single-molecule level. Our mMTT approach is based on exploiting the particular geometry of DNA-tethered magnetic beads under a cylindrical magnet with a small side magnet, which allows us to track rotation angle from the beads’ motion in $(X, Y)$. Using the mMTT implementation, we have obtained averaged extension-rotation and torque-rotation curves for DNA at varying salts and forces to, in particular, probe the effect of ionic conditions on the torsional stiffness of DNA. While we find the effective torsional stiffness to be ~5–10% smaller for higher salt concentrations for forces ~3 pN, $C_{\text{eff}}$ converges at high forces and there are no significant differences between salt conditions at 6.5 pN. The differences in the effective torsional stiffness at lower forces can be rationalized by mechanical models that only take into account the known change in the bending persistence length with salt and that assume a constant value for the intrinsic torsional stiffness of DNA. In summary, our results strongly suggest that while many properties of DNA under torsional strain, in particular of plectonemes, are salt-dependent, the intrinsic, high-force torsional stiffness of DNA is indepen-
dent of ionic strength. Our results provide fundamental input for models and simulations of DNA under torsional constraint and will be valuable for understanding DNA in more complex biological contexts.

Our multiplexed torque protocol opens up the possibility to probe small changes in nucleic acid mechanics, through averaging, which would be difficult to detect in ‘one-molecule-at-a-time’ measurements. Here, we have focused on the salt-dependence, but our method would be equally applicable to study e.g. anisotropic effects in bending and twisting or the temperature dependence of elastic properties. Going beyond bare DNA, multiplexed torque measurements will also be applicable to other molecules (e.g. double-stranded RNA (27)) and enable us to probe DNA–drug and DNA–protein interactions.

SUPPLEMENTARY DATA

Supplementary Data are available at NAR Online.

ACKNOWLEDGEMENTS

We thank Stefanos K. Nomidis and Enrico Carlon for providing the simulation data for the aTWLC model, Jelle van der Does for help with instrument development, Susanne Hage, Angelika Kardinal and Thomas Nicolaus for help with sample preparation, Stefan Ludwig for loan of the Hall probe and Theo Odijk for useful discussions.

FUNDING

German Research Foundation (DFG) via Nanosystems Initiative Munich (NIM) and Sonderforschungsbereich SFB 863 “Forces in Biomolecular Systems” (to J.L.); Interdisciplinary Center for Clinical Research (IZKF) at the University Hospital of the University of Erlangen-Nuremberg (to D.D.); European Research Council (ERC) via a Consolidation Grant (DynGenome, No 312221) (to N.H.D.); Funding for open access charge: Deutsche Forschungsgemeinschaft. Conflict of interest statement. None declared.

REFERENCES

1. Alberts, B., Bray, D., Lewis, J., Raff, M. and Roberts, K. (2002) Molecular Biology of the Cell. 4th edn. Garland Science, NY.
2. Watson, J.D. and Crick, F.H. (1953) Genetical implications of the structure of deoxyribonucleic acid. Nature, 171, 964–967.
3. Liu, L.F. and Wang, J.C. (1987) Supercoiling of the DNA template during transcription. Proc. Natl. Acad. Sci. U.S.A., 84, 7024–7027.
4. Vologodskii, A. (1994) DNA extension under the action of an external force. Macromolecules, 27, 5623–5625.
5. Borukhov, S. and Nudler, E. (2003) DNA polymerase holoenzyme: structure, function and biological implications. Curr. Opin. Microbiol., 6, 93–100.
6. Cozzarelli, N.R., Cost, G.I., Nöllmann, M., Viard, T. and Straß, J.E. (2006) Giant proteins that move DNA: bullies of the genomic playground. Nat. Rev. Mol. Cell Biol., 7, 580–588.
7. Roca, J. (2011) The torsional state of DNA within the chromosome. Chromosoma, 120, 323–334.
8. Castro, C.E., Kilchherr, F., Kim, D.-N., Shiao, E.L., Wauer, T., Wortmann, P., Bathe, M. and Dietz, H. (2011) A primer to scaffolded DNA origami. Nat. Methods, 8, 221–229.
9. Nelson, P. (2004) Biological Physics: Energy, Information Life. Freeman & Co, NY.
10. Kriegel, F., Ermann, N. and Lipert, J. (2016) Probing the mechanical properties, conformational changes, and interactions of nucleic acids with magnetic tweezers. J. Struct. Biol., 197, 26–36.
11. Smith, S.B., Finzi, L. and Bustamante, C. (1992) Direct mechanical measurements of the elasticity of single DNA molecules by using magnetic beads. Science, 258, 1122–1126.
12. Bustamante, C., Marko, J.F., Siggia, E.D. and Smith, S. (1994) Entropic elasticity of lambda-phage DNA. Science, 265, 1599–1600.
13. Cluzel, P., Lebrun, A., Heller, C., Lavery, R., Viovy, J.L., Chatenay, D. and Caron, F. (1996) DNA: an extensible molecule. Science, 271, 792–794.
14. Smith, S.B., Cui, Y. and Bustamante, C. (1996) Overstretching B-DNA: the elastic response of individual double-stranded- and single-stranded DNA molecules. Science, 271, 795–799.
15. Bryant, Z., Stone, M.D., Gore, J., Smith, S.B., Cozzarelli, N.R. and Bustamante, C. (2003) Structural transitions and elasticity from torque measurements on DNA. Nature, 424, 338–341.
16. Lionnet, T., Joubaud, S., Lavery, R., Bensimon, D. and Croquette, V. (2006) Wringing out DNA. Phys. Rev. Lett., 96, 178102.
17. Gore, J., Bryant, Z., Nöllmann, M., Le, M.U., Cozzarelli, N.R. and Bustamante, C. (2006) DNA overwinds when stretched. Nature, 442, 836–839.
18. Celedon, A., Nodelman, J.M., Wildt, B., Dewan, R., Seashore, P., Wirtz, D., Bowman, G.D. and Sun, S.X. (2009) Magnetic tweezers measurement of single molecule torque. Nano Lett., 9, 1720–1725.
19. Mosconi, F., Finzi, L., Bensimon, D. and Croquette, V. (2009) Measurement of the torque on a single stretched and twisted DNA using magnetic tweezers. Phys. Rev. Lett., 102, 078301.
20. Lipert, J., Kerssemakers, J.W.J., Jager, T. and Dekker, N.H. (2010) Magnetic torque tweezers: measuring torsional stiffness in DNA and RecA-DNA filaments. Nat. Methods, 7, 977–980.
21. Lipert, J., Donisch, S., Das, R. and Herschlag, D. (2014) Understanding nucleic acid-ion interactions. Ann. Rev. Biochem., 83, 813–841.
22. Odijk, T. (1977) Polyelectrolytes near the rod limit. J. Polym. Sci., 15, 477–483.
23. Skolnick, J. and Fixman, M. (1977) Electrostatic persistence length of a wormlike polyelectrolyte. Macromolecules, 10, 944–948.
24. Baumann, C.G., Smith, S.B., Bloomfield, V.A. and Bustamante, C. (1997) Ionic effects on the elasticity of single DNA molecules. Proc. Natl. Acad. Sci. U.S.A., 94, 6185–6190.
25. Wenner, J.R., Williams, M.C., Rouzina, I. and Bloomfield, V.A. (2002) Salt dependence of the elasticity and overstretching transition of single DNA molecules. Biophys. J., 82, 3160–3169.
26. Herrero-Galán, E., Fuentes-Perez, M.E., Carrasco, C., Valpuesta, J.M., Carrascosa, J.L., Moreno-Herrero, F. and Arias-Gonzalez, J.R. (2013) Mechanical identities of RNA and DNA double helices unveiled at the single-molecule level. J. Am. Chem. Soc., 135, 122–131.
27. Lipert, J., Skinner, G.M., Keegstra, J.M., Hensgens, T. and Bensimon, D. (2014) Double-stranded RNA under force and torque: similarities to and striking differences from double-stranded DNA. Proc. Natl. Acad. Sci. U.S.A., 111, 15408–15413.
28. Porschke, D. (1991) Persistence length and bending dynamics of DNA from electrooptical measurements at high salt concentrations. Biophys. Chem., 40, 169–179.
29. Barrat, J.L. and Joanny, J.F. (1993) Persistence length of polyelectrolyte chains. Europhys. Lett., 24, 333–338.
30. Barrat, J.L. and Joanny, J.F. (1996) Theory of polyelectrolyte solutions. Adv. Chem. Phys., 94, 1–66.
31. Baumann, C.G., Bloomfield, V.A., Smith, S.B., Bustamante, C., Wang, M.D. and Block, S.M. (2000) Stretching of single collapsed DNA molecules. Biophys. J., 78, 1965–1978.
32. Saveljev, A. and Papoian, G.A. (2006) Electrostatic, steric, and hydration interactions favor Na(+) condensation around DNA compared with K(+) . J. Am. Chem. Soc., 128, 14506–14518.
33. Mastroianni, A.J., Sivak, D.A., Geissler, P.L. and Alivisatos, A.P. (2009) Probing the conformational distributions of subpersistence length DNA. Nat. Rev. Mol. Cell Biol., 10, 1450–1458.
34. Saveljev, A., Materese, C.K. and Papoian, G.A. (2011) Is DNA’s rigidity dominated by electrostatic or nonelectrostatic interactions? J. Am. Chem. Soc., 133, 19290–19293.
