Cortical Transformation of Spatial Processing for Solving the Cocktail Party Problem: A Computational Model

Junzi Dong, H. Steven Colburn, and Kamal Sen

DOI: http://dx.doi.org/10.1523/ENEURO.0086-15.2015

Hearing Research Center and Department of Biomedical Engineering, Boston University, Boston, Massachusetts 02215

**Visual Abstract**

In multisource, “cocktail party” sound environments, human and animal auditory systems can use spatial cues to effectively separate and follow one source of sound over competing sources. While mechanisms to extract spatial cues such as interaural time differences (ITDs) are well understood in precortical areas, how such information is reused and transformed in higher cortical regions to represent segregated sound sources is not clear. We present a computational model describing a hypothesized neural network that spans spatial cue detection areas and the cortex. This network is based on recent physiological findings that cortical neurons selectively encode target stimuli in the presence of competing maskers based on source locations (Maddox et al., 2012). We demonstrate that key features of cortical re-
sponses can be generated by the model network, which exploits spatial interactions between inputs via lateral inhibition, enabling the spatial separation of target and interfering sources while allowing monitoring of a broader acoustic space when there is no competition. We present the model network along with testable experimental paradigms as a starting point for understanding the transformation and organization of spatial information from midbrain to cortex. This network is then extended to suggest engineering solutions that may be useful for hearing-assistive devices in solving the cocktail party problem.

Key words: auditory model of spatial processing; cocktail party problem; computational modeling; spatial auditory processing; spatial segregation

Introduction

The problem of recognizing and processing individual auditory objects in complex listening environments, the "cocktail party problem", was recognized over 50 years ago (Cherry, 1953); however, its neural mechanism remains poorly understood. Human and animal auditory systems selectively segregate and follow a selected sound source in the presence of competition to make sense of multiple-source environments (Bregman, 1994). Spatial cues enable listeners to segregate and follow individual sources, as demonstrated by human and animal studies (Hine et al., 1994; Dent et al., 1997, 2009; Darwin and Hukin, 1998; Arbogast et al., 2002). Although precortical neurons have been extensively shown to be selectively tuned to spatial cues, such as interaural time difference (ITD; Knudsen and Konishi, 1978; Yin and Chan, 1990; Peña and Konishi, 2001; Köppl and Carr, 2008; Devore et al., 2009), how spatial information from spatial cue detection areas is relayed to and used in higher cortical areas is not clear (Vonderschen and Wagner, 2014). Recent experiments on cortical responses revealed that whereas spatial tuning for single sound sources is broad, simultaneous competing sources increase spatial selectivity (Maddox et al., 2012; Middlebrooks and Bremen, 2013). Although these findings shed light on the spatial encoding capabilities of the cortex, neural mechanisms capable of generating such capabilities remain unknown. The goal of this study is to provide a computational model consistent with existing physiological evidence to describe the transformation between precortical areas and the cortex, which can selectively encode target stimuli when presented with competing sources in space. Specifically, we present a model network that replicates the spatial responses observed in a study by Maddox et al. (2012), providing a mechanistic solution to the spatial segregation of independent sources.

Maddox et al. (2012) demonstrated that, although the coding of song identity is not strongly impacted by stimulus location in quiet, location does have a significant effect on neural coding when there is a competing masker. In their experiments, two birdsongs were first presented independently from one of four stimulus locations (Fig. 1a). The neuron’s spatial performance was studied using the discriminability index, a metric quantifying the neural coding of song identity at each location. A larger difference in neural responses to the two songs gives higher song discriminability, indicating a location where birdsong is more “intelligible” to the neuron. For the target song alone (“clean”) case, similar discriminability across locations (Fig. 1a) indicates broad spatial tuning, where all spatial locations are similarly encoded within this neuron. In the masked conditions illustrated in Figure 1, b and c, a noise masker is played concurrently with a target, and the two are covaried in location for all possible combinations. A spatial discriminability grid of responses to all recorded target and masker location combinations (Fig. 1d) shows that for this unit, discriminability is better at a few “hotspots” shaded in lighter colors. These patterns indicate a sharpened spatial preference for encoded song stimuli in the presence of a competing masker at these locations.

In this paper, our goals are to construct a model network capable of replicating key features of the experimentally observed cortical responses: (1) similar discriminability for target songs in quiet at any location, indicating broad tuning and the ability of neurons to monitor the entire acoustic space in quiet; and (2) the emergence of hotspots where coding of song identity is enhanced at select stimulus locations in the presence of a second competing sound (the masker). The network can be adjusted to model a diverse range of spatial responses, demonstrated by fitting the population of neurons reported in the Maddox et al. (2012) study. Finally, we propose a way to extend this network to design engineering solutions that may be useful for achieving spatial stream segregation in hearing-assistive devices.

Methods

Network model overview

The network is composed of a three-layer structure, where the bottom layer receives precortical input, and the final layer provides the cortical output, which is then compared to the recordings. The model architecture, model mechanisms and parameters, and simulated precortical input are explained in separate sections below.
Network model architecture

The structure of the model, which was custom written in MATLAB, can be seen in Figure 2a–c. The basic architecture consists of an input layer with four spatial input channels corresponding to $-90^\circ$, $0^\circ$, $45^\circ$, and $90^\circ$ to mirror the experimental design of Maddox et al. (2012), and an intermediate layer of processing that includes excitatory relay neurons (R) and inhibitory neurons (I), and an output cortical neuron (C). The detailed network connectivity is determined by the additional lateral inhibitory

Figure 1. Recorded cortical neurons develop sharper spatial responses to targets when a noise masker is present (Maddox et al., 2012). a, Responses to target alone. Two bird songs—Song 1 and 2 (spectrograms shown in top left)—are played separately from four locations $-90^\circ$, $0^\circ$, $45^\circ$, and $90^\circ$. Recorded raster plots of responses to the two birdsongs are shown at each azimuth location. Positive degrees indicate locations contralateral to recording site. The color-coded discriminability values for each location are shown in the horizontal grid on the upper right. (Color map for all panels is shown in d, top row.) b, c, Responses to target with masker. Masker and one target song are played concurrently from one (colocated) or two (separated) of the four stimulus locations. A masker fixed at $0^\circ$ or $-90^\circ$, indicated by a black or grey boxed M, respectively, whereas the target song is played at one of the locations shown. As in a, recorded raster responses from each target location are shown, and discriminability values are shown in the colored grid of values (top right). d, Discriminability values for all location combinations. The top grid (single row) of numbers are the discriminability values for the “clean” (target-alone) conditions. In the lower, spatial discriminability grid, each block indicates a target and masker location combination. The rows indicated by a black or grey boxed M are cases where the masker is fixed at $0^\circ$ or $-90^\circ$. Blocks in all grids are colored according to the color scale given at the top of this panel.
Figure 2. Lateral inhibition in the model can account for the spatial tuning and spatial segregation properties of recorded units. 

**a–c,** Left, Model structure. Center, Simulated spatial grid. Right, Raster plots for stimulus conditions indicated by dashed or solid squares in the grid. Top right, Inset, The simulated discriminability for the clean (no-masker) case indicating broad spatial tuning. This clean case is not impacted by the addition of lateral inhibition, and is identical for all networks shown. 

**a,** Basic model structure with no lateral inhibitory connections. Simulated multisource spatial grid in model without lateral inhibition lacks the spatial diversity observed in the data. 

**b,** Spatial grid produced by the model with one inhibitory connection between 0° and –90°, shows an increase in discriminability when target and masker are presented at 0° and –90°, respectively. 

**c,** Model with additional inhibitory connections simulates the spatial response of the recorded unit shown in Figure 1d. 

**d,** Subthreshold responses of relay and cortical neurons, R1, R2, and C (b, left), for the labeled time segment (b, right) of one trial when target is presented at 0° and masker at –90°. Direct excitatory currents to R1 (R1 Conduc: black curve) are offset by inhibitory currents from I2 (R1 Conduc: magenta curve), and R1 is unable to reach spiking threshold, as seen in its voltage trace (R1 Voltage: black curve). In contrast, R2 is able to relay its temporal information to C, whose spiking pattern (C Voltage) resembles that of R2 (R2 Voltage).
connections as illustrated in Figure 2. Our goal was to match the response of the output cortical neuron C in the model to the main features of the neurons recorded in the experiments by Maddox et al. (2012).

**Biological rationale**

The convergence architecture was hypothesized based on physiological data showing selected spatial tuning responses in the midbrain (Knudsen and Konishi, 1978; Yin and Chan, 1990; Köppl and Carr, 2008), in contrast to the broad tuning observed in the cortex (Stecker et al., 2005; Higgins et al., 2010). The spectrototemperial response properties of the input layer neurons were modeled after experimentally measured spectrototemporal receptive fields (STRFs) of neurons in the avian midbrain (Amin et al., 2010; see Network model input). We modeled four spatial input channels as described above. In the biological system, there could be more input channels tuned at different locations at a finer spatial resolution. The spatial tuning of zebra finch midbrain neurons remains unknown. We began with the simplest assumption that there were no interactions across spatial input channels, and later relaxed this assumption to allow spatial overlap between the input channels and demonstrated that the model remains robust over a range of spatial overlaps (see Spatial tuning width at the input stage and Fig. 4).

This model architecture is consistent with the inhibitory (and relay) neurons being located anywhere in the processing stream between the input (midbrain) neurons and the output cortical neuron. It is possible that the inhibitory (and relay) neurons are located in the thalamus. Inhibitory neurons have been found at the thalamic level in birds (Pinaud and Mello, 2007) and some mammals (Winer, 1992). Alternatively, inhibitory (and relay) neurons might be located within cortex prior to the output cortical neuron. There is extensive evidence supporting the presence of inhibitory neurons at the cortical level, both in birds and mammals (Pinaud and Mello, 2007; Oswald et al., 2006).

**Model neurons**

All neurons in the model are integrate-and-fire neurons. Specific parameters used are described below. Resting potential was −60 mV, spiking threshold was −40 mV, and the reversal potential for excitatory currents was 0 mV for all neurons. In relay neurons, the reversal potential for inhibitory currents was −70 mV. In interneurons, EPSC was modeled as an alpha function with a time constant of 1 ms. In relay neurons, both EPSC and IPSC were modeled as the difference of a rising and a falling exponential, where rise and fall time constants were 1 and 3 ms, and 4 and 50 ms, respectively. An absolute refractory period of 3 ms was enforced in all neurons. These values are physiologically plausible (Froemke et al., 2007). In the cortical neuron, spike-rate adaptation was implemented by a hyperpolarizing conductance term that increases after firing and then recovers to zero exponentially (Dayan and Abbott, 2001). The adaptation time constant was 400 ms, and the strengths of the adaptation conductance for simulated neural units are shown in Table 1. Input synapses to the cortical neuron also have synaptic depression, which were modeled as described by Varela et al. (1997).

Table 1. STRFs input and adaptation conductance used for each simulated neural unit

| STRF no. | Neural units                          | Adaptation conductance |
|---------|--------------------------------------|------------------------|
| 1       | 3, 6, 9, 10, 11, 13, 21, 23           | 0.025                  |
|         | 14, 22                               | 0.04                   |
| 2       | 15                                   | 0                      |
| 3       | 29                                   | 0.12                   |
|         | 27                                   | 0.1                    |
| 4       | 7                                    | 0.07                   |
| 5       | 19                                   | 0.06                   |
| 6       | 2                                    | 0.06                   |
| 7       | 5                                    | 0.2                    |
| 8       | 20, 32                               | 0.07                   |
|         | 1, 12, 33                            | 0.08                   |
| 9       | 16, 23                               | 0.09                   |
| 10      | 8                                     | 0.09                   |
| 11      | 4                                     | 0.09                   |
| 12      | 26, 28, 31                           | 0.03                   |
| 13      | 17                                   | 0.01                   |
| 14      | 18                                   | 0.03                   |

STRF input and adaptation conductance were fit to best match the firing characteristics of each neuron recorded in the Maddox et al. (2012) study, whereas other neuron modeling parameters were fixed as reported above.

Although this quantitative formulation was applied to visual cortical synapses in Varela et al. (1997), synaptic depression is also observed in auditory thalamocortical circuits (Atzori et al., 2001; Rose and Metherate, 2005; Oswald et al., 2006; Levy and Reyes, 2012). We used a single synaptic depression component with fixed time course of 80 ms, and synaptic depression factor of 0.95, to model the experimental data by Maddox et al. (2012). Both adaptation and synaptic depression were implemented in the simulations shown in Figures 2 and 4 for all modeled neurons.

**Parameter fitting**

Parameters were held constant throughout all simulations, except for the synaptic strengths and the strength of neural adaptation. To fit each recorded neuron, we first fit the general neural dynamics and baseline discriminability values by adjusting the strength of neural adaptation and the synaptic strengths without lateral inhibition. The specific values of neural adaptation used can be found in Table 1. The feedforward synaptic weights (input to relay neuron) were then adjusted to match the discriminability values for clean and co-located cases at each azimuth, whereas other parameters were held the same. For lateral inhibition, the synaptic strength of each inhibitory connection was chosen to model the recorded discriminability of its corresponding song and masker location. Our goal in this study was to fit the spatial discriminability grids observed experimentally.

**Network model input**

The model input is composed of four spatial input channels corresponding to the stimulus locations used in the experiment by Maddox et al. (2012) (Fig. 2). Each channel receives simulated spike train responses of neurons at midbrain level as input. Input responses were simulated with STRFs modeled after typical STRFs obtained from...
the midbrain (MLd) of zebra finch songbirds (Amin et al., 2010). The input generation process is illustrated in Figure 3 and explained in detail below. For the majority of simulations, the azimuth response field for each modeled neuron was simulated with a Gaussian function, and across the population, there was minimal overlap between response fields. (Fig. 4, bottom left). This no-overlap assumption effectively means that for the azimuth locations used in the experiment, neighboring sources are outside the spatial receptive field, and each input channel will only respond to stimuli from its corresponding location. The effect of wider spatial tuning was also studied by running separate simulations with wider, overlapping Gaussian inputs (see Results).

**Model input using STRFs**

STRFs were used to simulate input responses. These STRFs were modeled using the product of Gabor functions in the time and frequency domain (Qiu et al., 2003):

\[
\text{STRF}(t, f) = G(t) \cdot H(t),
\]

where

\[
G(t) = e^{-0.5(t-t_0)^2/\alpha^2} \cdot \cos[2\pi \cdot \Omega_t \cdot (t - f_0)],
\]

and

\[
H(t) = e^{-0.5(t-t_0)^2/\alpha^2} \cdot \cos[2\pi \cdot \Omega_t \cdot (t - t_0) + P_t].
\]

The frequency range is determined by \( f_0 \), the best frequency; \( \alpha \), the spectral bandwidth; and \( \Omega_t \), the best temporal modulation frequency, which were chosen and fixed at 4300 Hz, 2000 Hz, and 50 \( \mu \)s, respectively, to generate a broadband STRF for all simulations based on physiological ranges reported in the MLd of zebra finch songbirds by Amin et al. (2010). Temporal parameters \( t_0 \), the temporal latency; \( \sigma_t \), the temporal bandwidth; and \( \Omega_t \), the best temporal modulation frequency, were assigned 7 ms, 4.5 ms, and 56 Hz, respectively, based on recorded physiological values (Amin et al., 2010).

The normalization factor and temporal phase (\( P_t \)) were varied to match the neuron-specific raster responses seen in the neural recordings of the Maddox et al. (2012) study. Other STRF parameters were largely fixed for simplicity, but the model is robust to variations in these parameters. Specific values of used parameters are shown in Table 2.

**STRF modeled input spike trains**

As shown in Figure 3, STRFs were first converted to firing rates by convolving the stimulus spectrogram with the model STRF and half-wave rectifying so that rate outputs were positive. For each simulated neuron, the firing rate was normalized by factor \( a \) to adjust the final mean firing rate: \( r(t) = a \cdot r(t) \). Finally, a Poisson spike model with a refractory period of 6 ms generated the neural response spikes used as the network model inputs, consistent with the instantaneous rates.

**Spatial tuning width at the input stage**

Spatial tuning width at the midbrain level varies across species, and is notably broader relative to the behavioral tuning for some mammals (Vonderschen and Wagner, 2014). To investigate whether the network model is functionally feasible with broader spatial tuning, the effect of spatial tuning width variation was studied by running simulations on an example neural unit and its neural network. The spatial tuning curves of input neurons were assumed to be Gaussian functions with varying standard deviations (SD), as shown in Figure 4. Tuning widths (twice the SD \( \sigma \)) of 15° or smaller result in no crosstalk between the input channels separated by 45°, as implemented in the main experiment. For the model unit used to test the effect of overlap (Table 1, unit 2), the tuning was then increased to show differences in model responses.

**Table 2. Parameters used for each type of input model STRF**

| STRF no. | Normalization factor | \( P_t \) (rad) |
|---------|----------------------|-----------------|
| 1       | 0.08                 | 1.4608          |
| 2       | 0.1                  | 1.4923          |
| 3       | 0.07                 | 1.508           |
| 4       | 0.1                  | 1.5237          |
| 5       | 0.12                 | 1.5394          |
| 6       | 0.1                  | 1.5425          |
| 7       | 0.07                 | 1.5425          |
| 8       | 0.087                | 1.5582          |
| 9       | 0.15                 | 1.5582          |
| 10      | 0.05                 | 1.5598          |
| 11      | 0.08                 | 1.5708          |
| 12      | 0.16                 | 1.5708          |
| 13      | 0.17                 | 1.5708          |

Temporal phase \( P_t \) and normalization factor are adjusted to match the recorded responses of the corresponding neurons, while other temporal and spectral parameters are held fixed and reported above.
Discriminability index: evaluating stimulus encoding and spatial tuning

The discriminability index calculates the level of dissimilarity between spike trains generated in response to two songs (Wang et al., 2007). For both sets of ten spike trains recorded from the same neuron, a random spike train from each song is chosen as a template, and the remaining spike trains are assigned to the closest template based on the van Rossum spike distance metric, which measures discrimination between two spike trains (van Rossum, 2001). This yields a perfect discriminability of 100% for an ideal response pair, and a chance discriminability of 50% for an indiscriminable response pair.

Quantifying goodness of fit

To assess the fit of the model to individual units from the original study, we calculated the average deviation and correlation coefficient between the discriminability values for clean and masked responses of the data and that of the simulation. The average deviation is the mean value of the absolute difference between each corresponding discriminability value.

Results

Cross-channel lateral inhibition enables the network to match experimentally observed neural responses

As described in Materials and Methods, a multilayer network model (Fig. 2a, left) of integrate-and-fire neurons was constructed to replicate selective spatial responses to competing sound sources. Input layer neurons represent neurons at the spatial cue detection level, and receive input generated by the model in Figure 3 when a stimulus is presented at the corresponding location (see Materials and Methods). Thus, there are four input “channels” corresponding to each speaker location in the experiment. The four input units excite four corresponding channels of relay neurons and interneurons in the middle-layer, which inherit their spatial tuning. Relay neurons converge to excite the cortical neuron (Fig. 2a, left), making it broadly tuned to stimuli from all directions in the clean (i.e., no masker) case (Fig. 2a, inset, discriminability grid), as observed in the data (Fig. 1a; see Materials and Methods, Network Model Architecture). However, in this
network (Fig. 2a, left), the spatial discriminability grid is relatively uniform (Fig. 2a, center column), unlike that observed in the data (Fig. 1d). Thus, this basic network replicates the broad response in the target alone case, but fails to produce the configuration-dependent hotspots observed in the data.

Introducing lateral inhibition from inter-neurons across spatial channels allows the target response to suppress the masker response when presented at the tuned locations, generating a hotspot of performance for a given target and masker location combination (Fig. 2b). Figure 2d depicts the subthreshold conductance and voltage changes in the relay and cortical neurons in the expanded time segment. Whereas neuron R2 spikes predictably in response to increases in EPSC, R1 is unable to spike following its EPSC input due to long-lasting suppression by lateral inhibition as seen in the increase in IPSC (Fig. 2d, bottom, magenta trace) from 12. In this case, the voltage response of the cortical neuron resembles that of R2 and the 0° target input (Fig. 2d). This is seen in the raster plots for the same stimulus paradigm, which resembles the target alone condition (Fig. 2b, bottom right), indicating that the cortical neuron is able to follow the target and largely ignore the masker. Note that when the locations of target and masker are reversed, discriminability decreases due to the masking of target by noise (Fig. 2b, center and top right). The preferred spatial location combinations in the recorded unit (Fig. 1d) can be modeled by introducing additional lateral inhibitory connections as shown in Figure 2c.

By adjusting model parameters, we were able to satisfactorily fit 32 of 33 units recorded in the original study. The model was largely robust in the parameter ranges we tested (see Materials and Methods for details). We used two parameters to assess the closeness of fit between each unit and its model simulation. Average deviation measures the closeness of the discriminability values of the simulation compared with the data in units of discriminability percentage, and was 3.39±0.97% for all simulated units. The correlation coefficient ranging from −1 to 1 measures how closely the pattern of the simulated grid agrees with the experimental grid, and was 0.94±0.04 for the simulated units. The neural unit that did not have an overall satisfactory fit had a spatial grid that was very uniform, where discriminability variations within the grid were small and random. As a result, the simulated fit had a deviation value within the normal range, but a very low cross-correlation coefficient.

It is noteworthy that the model network without lateral inhibition showed a relatively uniform spatial grid (Fig. 2a, center column), unlike the experimental data. This network did include adaptation and synaptic depression (see Materials and Methods, Model neurons). Thus, without lateral inhibition, adaptation and synaptic depression are not sufficient to explain the experimentally observed hotspots in the spatial grid.

Spatial tuning
The sharpness of spatial tuning curves was varied to test whether the model can describe the data with broader spatial input at the midbrain level. In the initial simulations, we assumed no crosstalk between spatial channels, which corresponds approximately to a Gaussian spatial tuning curve of width $2\sigma$ (twice the SD $\sigma$) <15°, where $\sigma$ is the SD of the Gaussian function. As the width increased, more and more overlap occurred between channels, as shown in the left column of Figure 4a.

For the simulations shown in Figure 4, spatial tuning width $2\sigma$ was increased to 40°, 80°, and 120°, respectively, while keeping all other parameters identical. The results of broadened tuning widths are shown in Figure 4b,c. The goodness of fit, as quantified by deviation and cross-correlation coefficient, diminished as tuning width was broadened. The mean and standard deviation of these two measures calculated from the population of simulated units, is plotted as dotted lines and shaded areas in Figure 4b for reference. In the 40° case, both deviation and cross-correlation coefficient remain within the range for the population of simulated units. The spatial tuning grid for 40° seen in Figure 4c (bottom), also maintains the general features of the data (Fig. 1d) and the original minimum overlap simulation (Fig. 2c, center). Therefore, this network model remains robust when spatial tuning width is increased to 40°. Even at a spatial tuning width of 80°, which corresponds to a fairly large overlap, the correlation coefficient remains relatively high at 0.91 and the deviation relatively low at 6.42% (Fig. 4b). Thus, the model remains robust for spatially overlapping tuning curves, degrading gracefully at very high overlaps (eg, 120°; Fig. 4c, top).

Extending the model network to potential engineering solutions for segregating spatial sound sources
The network can be extended to provide an engineering solution to the problem of segregating target from noise in space for the maximal number of locations on the grid. Figure 5a demonstrates a network where good discriminability is obtained for all conditions with target location to the right of masker location. This network, together with a complementary network with high performance for grid positions above the diagonal, allows the segregation of non-colocated sources for any azimuth, while maintaining consistently high intelligibility when only one source is present. An alternative engineering solution is demonstrated in Figure 5b, where one channel acts as a beamformer by inhibiting all other channels. In this case, similar networks beaming at other directions will enable a user to selectively listen to any direction of interest.

Discussion
The network model used here provides an explicit way of generating neural responses that replicate the key features of the cortical neurons recorded by Maddox et al. (2012), and provides a neural strategy for transforming information into selective coding for sound sources in the presence of multiple sources. The network uses information from input neurons through individual spatial channels and matches the key experimental features through
convergent excitation and lateral inhibition across spatial channels.

Predictions and implications

Lateral inhibition
The model suggests that lateral inhibition plays an important role in spatial sound source segregation. While lateral inhibition is a widely known mechanism in the brain, to our knowledge this study is the first to demonstrate how it can be exploited in the context of the cocktail party problem. Inhibition is present in field L, as well as the mammalian primary auditory cortex (Müller and Scheich, 1988; Wehr and Zador, 2003). Recently, there has been evidence of suppression by spatially separated stimuli in the cortex of marmoset monkeys (Zhou and Wang, 2012, 2014), which could be a manifestation of the lateral inhibition postulated in the model.

Given this network, we propose a physiological experiment that may provide additional insights. One can experimentally test the nature and source of inhibition by locally blocking GABA receptors and measuring the spatial grid under the same experimental setup. If the recorded spatial grid becomes less spatially sensitive, the proposed lateral inhibitory connections are most likely local.

Exploring alternate mechanisms for spatial sound source segregation
The above simulations show that the sharpened spatial tuning in the presence of multiple sources, which allows for spatial stream segregation, can be achieved via lateral inhibition across spatial channels. An alternate mechanism for spatial streaming, proposed in a recent study (Middlebrooks and Bremen, 2013) is forward masking. Candidate neural mechanisms underlying forward masking are adaptation and synaptic depression. The network model used here incorporated both of these mechanisms to model the temporal dynamics of the cortical responses. Our simulations indicate that although these mechanisms are important in determining the temporal dynamics of neural responses, they alone fail to produce the diverse spatial grids seen in the Maddox et al. (2012) study because of a lack of cross-channel spatial interactions (Fig. 2a, middle). In particular, without lateral inhibition, the model does not replicate the hotspots seen in the experimentally observed spatial grid. Thus, lateral inhibition involving interactions across spatial channels is necessary in the model for replicating the spatial properties in the observed data.

Response to multiple maskers
For each recorded unit, looking at its single-masker spatial grid response provides predictions for how it might respond to multiple maskers. In Figure 2c, for example, the simulated neuron is robust to maskers presented from both −90° and 90° (independently) when the target is located at 0°. This is achieved in the model network by inhibitory connections from 0° to −90° and 90°, which means that target stimuli at 0° could mask two simultaneous noise sources from −90° and 90°. Consistent with this intuition, our simulated network for this unit was robust to simultaneous maskers from −90° and 90°. It should be possible to test such predictions by performing two-masker experiments physiologically, and comparing the results to those of single-masker cases for each neuron.
Potential engineering solution to the cocktail party problem

The engineering solution visualized in Figure 5b is robust to simultaneous maskers in all channels other than the target (in this case 3 simultaneous maskers at -90°, 45°, and 90°), making this a particularly attractive design option in the context of hearing assistive devices in the presence of multiple speakers.

We plan to use the proposed engineering solution networks in Figure 5 to segregate mixed-source acoustic stimuli by building a system that can take mixed-source acoustic inputs and output a single desired acoustic source. This will require two additional processing steps. First, a peripheral model that converts acoustic stimuli into neural representations consistent with the network input is needed. This will be a model where neurons selectively respond to a preferred direction using interaural cues, similar to previous neural models of spatial tuning (Fischer et al., 2009). Second, the neural network output, ie, spike trains representing the single desired source, needs to be converted back into acoustic waveforms. This can be done using stimulus reconstruction (Mesgarani and Chang, 2012). We are working on both steps with the long-term goal of ultimately testing the segregation capabilities of the model on normal and hearing-impaired listeners.

Spatial tuning of inputs and applicability of model to spatial processing in birds and mammals

For the majority of simulations, input neurons are assumed to have non-overlapping Gaussian spatial tuning curves centered at azimuths corresponding to those used in the experiment. A separate set of simulations showed that the model network remains robust when the spatial tuning curves are broadened to have significant overlap.

Spatially selective neurons found in the owl midbrain (Knudsen and Konishi, 1978; Peña and Konishi, 2001) and chicken hindbrain (Köppl and Carr, 2008) demonstrate ITD sensitivity within the physiological range. Although spatial tuning of midbrain neurons in the zebra finch remains unknown, it is likely that the auditory periphery contains similarly spatially sensitive neurons like other avian species, as spatial tuning appears to follow an evolutionary divide across species (Schnupp and Carr, 2009; Ashida and Carr, 2011). An outstanding question is whether the model will hold for species whose midbrain neurons show broader spatial sensitivity, such as small-headed mammals where tuning curves span an entire hemisphere or more (Vonderschen and Wagner, 2014). As we tested, the selective mechanism remains robust when spatial tuning is widened up to 40° (Fig. 4), comparable with some azimuth ITD tuning functions recorded in the rabbit IC by Day et al., (2012).

In species that show broad spatial tuning in the midbrain, spatial tuning may be further sharpened within the cortical level. One possibility is that broad spatially tuned precortical inputs are sharpened by a high threshold at the cortical level. A second possibility is that the spatial tuning of cortical neurons is sharpened during active engagement in a task (Lee and Middlebrooks, 2011).
ing solutions discussed in the paper and test whether the proposed circuit can successfully segregate sounds sources and improve listening performance in normal and hearing impaired listeners in cocktail-party-like settings.

References
Amin N, Gill P, Theunissen FE (2010) Role of the zebra finch auditory thalamus in generating complex representations for natural sounds. J Neurophysiol 104:784–798. CrossRef Medline
Arbogast TL, Mason CR, Kidd G Jr (2002) The effect of spatial separation on informational and energetic masking of speech. J Acoust Soc Am 112:2086–2098. CrossRef
Ashida G, Carr CE (2011) Sound localization: Jeffress and beyond. Curr Opin Neurobiol 21:745–751. CrossRef Medline
Atzori M, Lei S, Evans DIP, Kanold PO, Phillips-Tansley E, McIntrye O, McBain CJ (2001) Differential synaptic processing separates stationary from transient inputs to the auditory cortex. Nat Neurosci 4:1230–1237. CrossRef
Bregman AS (1994) Auditory scene analysis: the perceptual organization of sound. Cambridge, MA: MIT.
Cherry EC (1953) Some experiments on the recognition of speech, with one and with two ears. J Acoust Soc Am 25:975. CrossRef
Darwin C, Hukin R (1998) Auditory objects of attention. J Acoust Soc Am 103:2928. CrossRef
Day ML, Koka K, Delgutte B (2012) Neural encoding of sound source location in the presence of a concurrent, spatially separated source. J Neurophysiol 108:2621–2628. CrossRef Medline
Dayan P, Abbott LF (2001) Integrating-and-fire models: spike-rate adaptation and refractoriness. In: Theoretical neuroscience: computational and mathematical modeling of neural systems, pp 165–166. Cambridge, MA: MIT.
Dent ML, Larsen ON, Dooling RJ (1997) Free-field binaural unmasking in budgerigars. Behav Neurosci 111:590–598. CrossRef
Dent ML, McClaine EM, Best V, Ozmeral E, Narayan R, Gallun FJ, Sen K, Shinn-Cunningham BG (2009) Spatial unmasking of bird-song in zebra finches and budgerigars. J Comp Psychol 123:357. CrossRef
Devore S, Ishfeld K, Hancock K, Shinn-Cunningham B, Delgutte B (2009) Accurate sound localization in reverberant environments is mediated by robust encoding of spatial cues in the auditory midbrain. Neurosci 62:123–134. [PMC] [10.1016/j.neuron.2009.02.018] [19376072] CrossRef
Fischer BJ, Anderson CH, Peña JL (2009) Multicategorical auditory spatial receptive fields created by a hierarchy of population codes. PloS One 4:e8015. CrossRef Medline
Froemke RC, Merzenich MM, Schreiner CE (2007) A synaptic memory trace for cortical receptive field plasticity. Nature 450:425–429. CrossRef Medline
Higgins NC, Storace DA, Escabi MA, Read HL (2010) Specialization of binaural responses in ventral auditory cortices. J Neurosci 30:14522–14532. CrossRef Medline
Hine JE, Martin RL, Moore DR (1994) Free-field binaural unmasking in ferrets. Behav Neurosci 108:196. Medline
Knudsen EI, Konishi M (1978) A neural map of auditory space in the owl. Science 200:795–797. Medline
Köppl C, Carr CE (2008) Maps of interaural time difference in the chicken’s brainstem nucleus laminaris. Biol Cybern 98:541–559. CrossRef Medline
Lee CC, Middlebrooks JC (2011) Auditory cortex spatial sensitivity sharpens during task performance. Nat Neurosci 14:108–114. CrossRef Medline
Levy RB, Reyes AD (2012) Spatial profile of excitatory and inhibitory synaptic connectivity in mouse primary auditory cortex. J Neurosci 32:5609–5619. CrossRef Medline
Maddox RK, Billimoria CP, Perrone BP, Shinn-Cunningham BG, Sen K (2012) Competing sound sources reveal spatial effects in cortical processing. PLoS Biol 10:e1001319. CrossRef Medline
Mesgarani N, Chang EF (2012) Selective cortical representation of attended speaker in multi-talker speech perception. Nature 485:233–236. CrossRef Medline
Middlebrooks JC, Bremen P (2013) Spatial stream segregation by auditory cortical neurons. J Neurosci 33:10986–11001. CrossRef Medline
Müller C, Scheich H (1988) Contribution of GABAergic inhibition to the response characteristics of auditory units in the avian forebrain. J Neurophysiol 59:1673–1689. Medline
Oswald AM, Schiff ML, Reyes AD (2006) Synaptic mechanisms underlying auditory processing. Curr Opin Neurobiol 16:371–376. CrossRef Medline
Peña JL, Konishi M (2001) Auditory spatial receptive fields created by multiplication. Science 292:249–252. CrossRef Medline
Pinaud R, Mello CV (2007) GABA immunoreactivity in auditory and song control brain areas of zebra finches. J Chem Neuroanat 34:1–21. CrossRef Medline
Qiu A, Schreiner CE, Escabi MA (2003) Gabor analysis of auditory midbrain receptive fields: spectro-temporal and binaural composition. J Neurophysiol 90:456–476. CrossRef Medline
Rose HJ, Metherate R (2005) Auditory thalamocortical transmission is reliable and temporally precise. J Neurophysiol 94:2019–2030. CrossRef Medline
Schnupp JW, Carr CE (2009) On hearing with more than one ear: lessons from evolution. Nat Neurosci 12:692–697. CrossRef Medline
Sen K, Theunissen FE, Doupe AJ (2001) Feature analysis of natural sounds in the songbird auditory forebrain. J Neurophysiol 86:1445–1458. Medline
Stecker GC, Harrington IA, Middlebrooks JC (2005) Location coding by opponent neuronal populations in the auditory cortex. PLoS Biol 3:e78. CrossRef Medline
van Rossum MC (2001) A novel spike distance. Neural Comput 13:751–763. Medline
Varela JA, Sen K, Gibson J, Fost J, Abbott LF, Nelson SB (1997) A quantitative description of short-term plasticity at excitatory synapses in layer 2/3 of rat primary visual cortex. J Neurosci 17:7926–7940. Medline
Wendelken K, Wagner H (2014) Detecting interaural time differences and remodeling their representation. Trends Neurosci 37:289–300. CrossRef Medline
Wang L, Narayan R, Grana G, Shamir M, Sen K (2007) Cortical discrimination of complex natural stimuli: can single neurons match behavior? J Neurosci 27:582–589. CrossRef Medline
Wehr M, Zador AM (2003) Balanced inhibition underlies tuning and sharpness tuning in auditory cortex. Nature 426:442–446. CrossRef
Winer JA (1992) The functional architecture of the medial geniculate body and the primary auditory cortex. In: The mammalian auditory pathway: neuroanatomy, p 287. Berlin: Springer-Verlag.
Yin T, Chan J (1990) Interaural time sensitivity in medial superior olives of cat. J Neurophysiol 64:465–488. Medline
Zhou Y, Wang X (2012) Level dependence of spatial processing in reverberant environments. J Neurophysiol 108:810–826. CrossRef Medline
Zhou Y, Wang X (2014) Spatially extended forward suppression in primate auditory cortex. Eur J Neurosci 919–933. CrossRef