Next-generation neural field model: The evolution of synchrony within patterns and waves

Áine Byrne*
Center for Neural Science, New York University, New York, New York 10003, USA
and Centre for Mathematical Medicine and Biology, School of Mathematical Sciences, University of Nottingham, University Park, Nottingham, NG7 2RD, United Kingdom

Daniele Avitabile
Centre for Mathematical Medicine and Biology, School of Mathematical Sciences, University of Nottingham, University Park, Nottingham, NG7 2RD, United Kingdom
and Inria Sophia Antipolis Méditerranée Research Centre, MathNeuro Team, 2004 route des Lucioles, Bote Postale 93 06902 Sophia Antipolis, Cedex, France

Stephen Coombes
Centre for Mathematical Medicine and Biology, School of Mathematical Sciences, University of Nottingham, University Park, Nottingham, NG7 2RD, United Kingdom

(Received 7 September 2018; published 7 January 2019)

Neural field models are commonly used to describe wave propagation and bump attractors at a tissue level in the brain. Although motivated by biology, these models are phenomenological in nature. They are built on the assumption that the neural tissue operates in a near synchronous regime, and hence, cannot account for changes in the underlying synchrony of patterns. It is customary to use spiking neural network models when examining within population synchronization. Unfortunately, these high-dimensional models are notoriously hard to obtain insight from. In this paper, we consider a network of \( \theta \)-neurons, which has recently been shown to admit an exact mean-field description in the absence of a spatial component. We show that the inclusion of space and a realistic synapse model leads to a reduced model that has many of the features of a standard neural field model coupled to a further dynamical equation that describes the evolution of network synchrony. Both Turing instability analysis and numerical continuation software are used to explore the existence and stability of spatiotemporal patterns in the system. In particular, we show that this new model can support states above and beyond those seen in a standard neural field model. These states are typified by structures within bumps and waves showing the dynamic evolution of population synchrony.

DOI: 10.1103/PhysRevE.99.012313

I. INTRODUCTION

The act of passing information between brain regions produces waves of neural activity. These waves are readily observed using noninvasive techniques such as electroencephalography (EEG) and magnetoencephalography (MEG) [1], as well as in brain slices [2]. Both experimental and theoretical work has shown that EEG and MEG recordings and evoked potentials can exhibit traveling and standing waves [3]. In particular, traveling waves are seen in EEG sleep recordings propagating across the cortex at a speed of about 1.2–7.0 m/s [4]. Standing waves are often associated with idle brain states. For example, standing waves at \( \alpha \) frequency (8–13 Hz) are observed in the vicinity of the visual cortex when the subject has their eyes closed [5]. Another commonly observed spatial pattern is the so-called bump attractor. This spatially localized increase in population firing is produced in working memory tasks and the location of the bump can be linked to memory location [6].

Traditionally, neural field models are used to describe wave and bump states in the brain. Although inspired by biology, these models are entirely phenomenological in nature. Even so, they have been particularly successful in describing neurophysiological phenomena, such as EEG and MEG rhythms [7], working memory [8], binocular rivalry [9], and orientation tuning in the visual cortex [10]. They are typically cast as a system of nonlocal differential equations which describe the spatiotemporal evolution of coarse-grained population variables, such as the firing rate of a neuronal population, the average synaptic current, or the mean membrane potential [11].

The first attempt at a neural field mode is attributed to Beurle [12], who built a model to describe the propagation of activation in a given volume of neural tissue. This model was purely excitatory, but even so allowed him to examine the propagation of large-scale brain activity. In the 1970s Wilson and Cowan [13,14] extended this model to include a second inhibitory layer. Unlike Beurle, they were interested in spatially localized bump solutions. In his seminal paper, Amari [15,16] created what is now known as the standard neural field equation. By introducing a Mexican hat–type
coupling function (local excitation and long-range inhibition), he reduced the model to a single equation with a mixture of excitatory and inhibitory connections. This allowed him to construct explicit solutions for spatially localized patterns and assess their stability (at least for a Heaviside firing rate function). For a review of the Amari model and bumps in one spatial dimension, see Ref. [17], and for a discussion of bubbles in two spatial dimensions, see Ref. [18].

One of the main assumptions in many types of neural field models, and especially those for describing EEG, is that pointwise they describe a density of neurons operating in a near synchronous regime [19]. This wholly reasonable assumption can be traced back to the observation that an EEG scalp electrode, which typically experiences the activity of roughly $10^9$ cortical pyramidal cells, can only detect an electric field if all the individual cell dipoles add coherently [20]. However, a near synchrony assumption in any neural mass model precludes its use in describing the increase and decrease of power commonly seen in given EEG and MEG frequency bands. These temporal variations are believed to be the result of changes in synchrony within the neural tissue. The former phenomenon is called event-related synchronization (ERS), and the latter event-related desynchronization (ERD) [21]. Consequently, there is a pressing need to develop the next generation of neural field models, which include this notion of a dynamic within-population synchrony (not fixed to be near synchronous), to more accurately describe the evolution of large-scale spatiotemporal brain rhythms.

When looking at within-population synchronization one typically uses a spiking neural network model. However, these high-dimensional models are almost impossible to gain insight from. In an ideal world there would be a mathematical procedure for linking microscopic dynamics to macroscopic dynamics. This link has proved elusive for the majority of spiking models. However, Luke et al. [22] showed that the θ-neuron model is amenable to such a reduction for pulsatile coupling. Montbrió et al. [23] used a similar approach to reduce a network of quadratic integrate-and-fire neurons. Laing [24] has also shown that the same approach can be applied to a network of spatially extended θ-neurons, in the presence of gap junction coupling. In previous papers [25,26], we have shown that the approach of Luke et al. can be extended to incorporate a biologically realistic form of synaptic coupling. Here we build on this work to construct a neural field model that incorporates within population synchrony and a realistic form of synaptic coupling. We shall refer to this model as a next generation neural field model. Esmaola-Acebes et al. recently showed that a similar model of pulse-coupled excitatory and inhibitory quadratic integrate-and-fire neurons displayed damped temporal oscillations, which modulate a spatially nonlocalized profile [27]. Such oscillations are, however, not self-sustained. Here, we show, through the inclusion of synaptic dynamics, that the model can support self-sustained oscillations.

Unlike more traditional neural field models the one studied here has a population firing rate at a point in the tissue that depends on the degree of synchrony at that point. This firing rate is a real valued function of the complex Kuramoto order parameter, and as such different values of the order parameter can give rise to the same population rate. Thus, in contrast to phenomenological neural field models that are closed under the choice of a firing rate that is a nonlinear (typically sigmoidal) function of mean-membrane potential or synaptic activity, the one presented here is expected to have a richer set of responses, due to the more sophisticated representation of the response of the population rate to synchrony levels. This allows the model to represent underlying patterns of spike-train synchrony that cannot be accounted for in standard neural field models. In particular, we show, using a mixture of analysis and simulation, that this new neural field model can support exotic patterned states more reminiscent of high-dimensional spiking networks, with spatiotemporal patterns showing the evolution of synchrony.

We begin with an overview of the model formulation in Sec. II and outline the necessary steps for reduction to a neural field. A Turing instability analysis of the model is covered in Sec. III. Here, we show that the system can be unstable to both static and dynamic Turing patterns for a wide window of parameter space. More interestingly, we show that when the Turing bifurcation collides with a Hopf bifurcation patterned states emerge in which there exists an oscillating structure within a spatially localized bump. The Turing analysis is complimented with a numerical bifurcation analysis for the full nonlinear model in Sec. IV. Here we further examine the emergent patterns away from bifurcation, as well as consider localized traveling waves. Finally, in Sec. V we discuss our main results as well as natural extensions of the work presented.

II. THE MODEL

We first consider a network of $N$ coupled quadratic integrate-and-fire (QIF) neurons, uniformly distributed along a line of length $\Lambda$ such that the $j$th neuron is at position $x_j = -\Lambda/2 + (j-1)\Delta x$, where $j = 1, \ldots, N$ and $\Delta x = \Lambda/(N-1)$ is the spacing between neurons. The coupling between neuron $i$ and neuron $j$ depends only upon the distance between the two neurons, $w_{ij} = w_{ij}(|x_i - x_j|)$, where $w_{ij}$ is a label used to keep track of neural subpopulations. We write the network dynamics for the voltage, $v_i \equiv v(x_i,t)$, in the form

$$\dot{v}_i = v_i^r + \eta_i + I_i, \quad i = 1, \ldots, N,$$

subject to reset, $v_i \rightarrow v_r$, whenever a firing threshold $v_{th}$ is reached by $v_i$. The time at which the $i$th cell reaches threshold from below for the $s$th time will be denoted by $T^s_i$, $s \in \mathbb{N}$. Here the background drives $\eta_i$ will be assumed to be heterogeneous and chosen from a Lorentzian distribution,

$$L(\eta) = \frac{1}{\pi} \frac{\Delta}{(\eta - \eta_0)^2 + \Delta^2},$$

where $\eta_0$ is the center of the distribution and $\Delta$ is the half width. We assume a synaptic input current of the form

$$I_i(t) = \sum_m g_m^i(t)(v_{syn}^m - v_i(t)),$$

for a global conductance $g_m^i$, synaptic reversal potential $v_{syn}^m$ and local voltage $v_i$. In what follows we will assume $m = \{1,2\}$ or $m = 1$, but one should note that this framework can be extended to include multiple types of synapses. The interplay of excitation and inhibition, on different spatial...
scales, is known to play an important role in the generation of global spatially patterned states [28–30]. Hence, we separate our synaptic conductance into two parts, such that we have one excitatory synaptic current ($v_{\text{syn}} > 0$) and one inhibitory ($v_{\text{syn}} < 0$), each with different spatial ranges.

Each of the synaptic conductances will be taken to mimic that of a synapse with a finite rise and fall time that evolves \( "spikes" \) whenever \( vr_i \in R \). It is well known that the QIF model is formally equivalent to the \( \theta \)-neuron network dynamics as

\[
\theta_i = 1 - \cos \theta_i + (1 + \cos \theta_i) n_i + \sum_m g_m^i [1 + \cos \theta_i] v_{\text{syn}}^m - \sin \theta_i, \tag{6}
\]

Substituting Eq. (11) into the continuity Eq. (8) and balancing terms in \( e^{i\phi} \) gives an evolution equation for \( \alpha \):

\[
\frac{\partial}{\partial t} \alpha - i \alpha^2 \phi - i \alpha \chi - i \phi = 0. \tag{13}
\]

We define the Kuramoto order parameter as follows:

\[
z(x, t) = \int_0^{2\pi} \! d\theta \int_{-\infty}^{\infty} \! d\eta \rho(x, \eta, \theta, t) e^{i\eta}. \tag{14}
\]

where \( z \) denotes the complex conjugate of \( z \). As the Lorentzian has two simple poles \( \eta_{\pm} = \eta_0 \pm i \Delta \), the above integral may be performed by choosing a large semicircular contour in the lower half \( \eta \)-plane and using the residue theorem, to yield \( z(x, t) = \alpha(x, \eta, t) \).

We use Eq. (14) to write Eq. (10) as

\[
Q_w g_m(x, t) = \kappa_m \int_{-\infty}^{\infty} \! dy w_m(x - y) f[z(y, t)], \tag{16}
\]
where $\otimes$ represents a spatial convolution and $f$ is the population firing rate

$$f(z) = \frac{1}{\pi} \left[ 1 + \sum_{l=1}^{\infty} (-1)^l z^l + cc \right]$$

$$= \frac{1}{\pi} \left[ 1 - |z|^2 \right] \frac{1}{|1 + z|^2}, \quad |z| < 1.$$  

Note that Eq. (16) takes the form of a generalised neural field equation, where the firing rate function $f$ is a derived quantity that depends on the within population synchrony. Also noteworthy is the fact that this firing rate function is not a sigmoid. It is a highly nonlinear function that depends on the intrinsic population dynamics. The firing rate can be plotted as a function of the Kuramoto order parameter (Fig. 1). As expected, the firing rate is highest at $z = e^{i\alpha}$. This corresponds to highly synchronous behavior where all of the phases of the neurons go through $\pi$ simultaneously.

FIG. 1. Firing rate dynamics: Density plot showing the firing rate $f$ as a function of the complex Kuramoto order parameter $z = Re^{i\alpha}$. Firing is highest near $z = e^{i\alpha}$. This corresponds to highly synchronous behavior where all of the phases of the neurons go through $\pi$ simultaneously.

where $\otimes$ represents a spatial convolution and $f$ is the population firing rate

$$f(z) = \frac{1}{\pi} \left[ 1 + \sum_{l=1}^{\infty} (-1)^l z^l + cc \right]$$

$$= \frac{1}{\pi} \left[ 1 - |z|^2 \right] \frac{1}{|1 + z|^2}, \quad |z| < 1.$$  

Note that Eq. (16) takes the form of a generalised neural field equation, where the firing rate function $f$ is a derived quantity that depends on the within population synchrony. Also noteworthy is the fact that this firing rate function is not a sigmoid. It is a highly nonlinear function that depends on the intrinsic population dynamics. The firing rate can be plotted as a function of the Kuramoto order parameter (Fig. 1). As expected, the firing rate is highest at $z = e^{i\alpha}$. This corresponds to highly synchronous behavior where all of the phases of the neurons go through $\pi$ simultaneously.

where $\otimes$ represents a spatial convolution and $f$ is the population firing rate

$$f(z) = \frac{1}{\pi} \left[ 1 + \sum_{l=1}^{\infty} (-1)^l z^l + cc \right]$$

$$= \frac{1}{\pi} \left[ 1 - |z|^2 \right] \frac{1}{|1 + z|^2}, \quad |z| < 1.$$  

Note that Eq. (16) takes the form of a generalised neural field equation, where the firing rate function $f$ is a derived quantity that depends on the within population synchrony. Also noteworthy is the fact that this firing rate function is not a sigmoid. It is a highly nonlinear function that depends on the intrinsic population dynamics. The firing rate can be plotted as a function of the Kuramoto order parameter (Fig. 1). As expected, the firing rate is highest at $z = e^{i\alpha}$. This corresponds to highly synchronous behavior where all of the phases of the neurons go through $\pi$ simultaneously.

where $\otimes$ represents a spatial convolution and $f$ is the population firing rate

$$f(z) = \frac{1}{\pi} \left[ 1 + \sum_{l=1}^{\infty} (-1)^l z^l + cc \right]$$

$$= \frac{1}{\pi} \left[ 1 - |z|^2 \right] \frac{1}{|1 + z|^2}, \quad |z| < 1.$$  

Note that Eq. (16) takes the form of a generalised neural field equation, where the firing rate function $f$ is a derived quantity that depends on the within population synchrony. Also noteworthy is the fact that this firing rate function is not a sigmoid. It is a highly nonlinear function that depends on the intrinsic population dynamics. The firing rate can be plotted as a function of the Kuramoto order parameter (Fig. 1). As expected, the firing rate is highest at $z = e^{i\alpha}$. This corresponds to highly synchronous behavior where all of the phases of the neurons go through $\pi$ simultaneously.
all \( k \). By the implicit function theorem, a branch of solutions \( \lambda(k) \) to Eq. (23) touches the imaginary axis when

\[
\partial k \mathcal{M} \partial \omega \mathcal{N} - \partial \omega \mathcal{M} \partial k \mathcal{N} = 0,
\]

(24)

where \( \mathcal{M} = \text{Re}(\mathcal{E}) \) and \( \mathcal{N} = \text{Im}(\mathcal{E}) \).

We observe a Hopf bifurcation of the spatially uniform state \( u^* \) if Eq. (23) holds for \( \nu(0) = 0 \) and \( k = 0 \), i.e., if there is a nonzero solution of

\[
\omega^6 + p_4 \omega^4 + p_2 \omega^2 + p_0 = 0,
\]

(25)

\[
p_5 \omega^4 + p_3 \omega^2 + p_1 = 0.
\]

(26)

Here, \( p_i \) are scalars which depend on \( u_* \) and the control parameters of the problem (see Appendix B). Solving Eqs. (25) and (26), for fixed width of the Lorentzian \( \Delta \), synaptic coupling strengths \( \kappa_1, \kappa_2 \), synaptic time constants \( \tau_1, \tau_2 \), and relative width of the synaptic kernel \( \beta^{-1} \), gives the locus of Hopf bifurcations as a function of the synaptic reversal potential \( v_{\text{syn}} \) and background drive \( \eta_0 \) [Fig. 2(a), green curve]. We fix the synaptic reversal potentials to be equal and opposite, and define \( v_{\text{syn}} = v_{1,\text{syn}} = -v_{2,\text{syn}} \). For simplicity, we set \( \kappa_1 = \kappa_2 \) and \( \tau_1 = \tau_2 \). For this choice of parameters, excitation dominates for short-range interactions for \( v_{\text{syn}} > 0 \) and inhibition dominates for short-range interactions for \( v_{\text{syn}} < 0 \). Note, also, that the Hopf bifurcation occurs for the same value of \( \eta_0 \) for all \( v_{\text{syn}} \). This is a consequence of the choice of equal coupling strengths and time constants. If this balance is disrupted, the Hopf bifurcation will depend upon \( v_{\text{syn}} \) and for some parameter choices we see several Hopf curves in the \( (v_{\text{syn}}, \eta_0) \) plane.

The homogeneous steady state \( u^* \) undergoes a static Turing bifurcation if there exists a nonzero critical wave number \( k_c \) such that Eqs. (23) and (24) hold for \( \nu(k_c) = 0 \), \( \omega(k_c) = 0 \). This leads to the conditions

\[
p_0 + q_0 \tilde{\omega}_1 + q_0 \tilde{\omega}_1 = 0,
\]

(27)

\[
q_0 \frac{d \tilde{\omega}_1}{dk_c} + q_0 \frac{d \tilde{\omega}_1}{dk_c} (p_1 + q_1 \tilde{\omega}_1 + q_1 \tilde{\omega}_2) = 0,
\]

(28)

where \( \tilde{\omega}_i \) and its derivative depend on \( k_c \) and \( \beta \), and the scalars \( p_i, q_i \) depend on \( u_* \) and the control parameters of the problem (see Appendix B).

As with the Hopf bifurcation, the locus of Turing bifurcations can be plotted as a function of the synaptic reversal potential \( v_{\text{syn}} \) and background drive \( \eta_0 \) (Fig. 2, red curve). The curve exhibits a turning point, therefore the system has two Turing bifurcations for sufficiently large values of \( v_{\text{syn}} \). If we fix \( v_{\text{syn}} \) at a value in this region, and ascend the bifurcation diagram by increasing \( \eta_0 \), the spectrum \( \lambda(k) \) touches the imaginary axis of the \( (\nu, \omega) \) plane with wave number \( k_c \) (lower Turing bifurcation) [Fig. 2(c)] and continues to move to the right, implying that \( u^* \) is unstable to a range of perturbations with wave numbers \( k \in (k_1, k_2) \). As \( \eta_0 \) is further increased, the spectrum returns to the left-hand plane (upper Turing bifurcation), which restores the stability of \( u^* \). Note the value of \( k_c \) is not necessarily the same on the upper and lower branches. The scenario described above is
robust to perturbations in other parameters: we found that changes in $\tau_1$, $\tau_1$, and $\Delta$ do not significantly affect the location of the Turing bifurcations. Increasing $\kappa_2$ results in an increase of the gap between the two critical values of $\eta_0$, and hence a larger window of instability, while increasing $\kappa_1$ decreases this gap and at a certain point the shape is inverted, such that the unstable region lies predominantly in the $\eta_0 < 0$ region of the plot. As $\kappa_1$ corresponds to the synaptic strength for the excitatory current for $v$, changes in $\kappa_1$ dominantly results in an increase in the linearized operator around an equilibrium are solved simultaneously with Eqs. (25) and (26), (27) and (28), or (29)–(31) and continued in parameter space. The curves in Fig. 2(a) were computed using XPPAUT [35], by continuing a suitable algebraic problem in one of the parameters of the system $(v_{syn}, \eta_0)$. The equations defining an equilibrium are solved simultaneously with Eqs. (25) and (26), (27) and (28), or (29)–(31) and continued in parameter space. The curves partition the $(v_{syn}, \eta_0)$ space into five sectors (labelled I–V). In addition to sectors where $u^*$ is stable (I), $u^*$ is unstable to bulk oscillations (II), Turing instabilities (III), and Turing-Hopf instabilities (IV), a fifth sector (V) is generated by the crossing of the Turing and Hopf curves. At the intersection (codimension-2) point, the spectrum of the linearized operator around $u^*$ has one zero eigenvalue and two complex conjugate eigenvalues, where the critical wave number $k_c$ is nonzero for the zero eigenvalue and equal to zero for the complex conjugate pair [Fig. 2(e)]. Direct numerical simulations close to the instability confirm the predictions of the linear stability analysis: bulk oscillations are observed in in Sec. I [Fig. 2(b)] stationary Turing patterns are observed in sector III [Fig. 2(c)] and both wave trains and standing waves are seen in region IV [Fig. 2(d)]. In sector V, the simultaneous Turing and Hopf unstable modes compete, resulting in a characteristic complex spatiotemporal pattern, where temporal oscillations develop within each bump of a Turing pattern [Fig. 2(e)]. The existence of the intersection point of the Turing and Hopf curves and the observation of the spatiotemporal patterns are robust to changes in parameters. In passing we note that, close to onset, we could find only large amplitude patterns of the type shown in Figs. 2(e)–2(e), indicating that the Turing and Turing-Hopf bifurcations are subcritical (as confirmed below by numerical continuation). Interestingly, we also observe dynamic Turing patterns in region II, implying that the Hopf bifurcation does not stabilize the system, instead it creates bistability in this region, where the system supports both bulk oscillations and dynamic global patterns.

We also found other complex spatiotemporal patterns away from bifurcation onset, using direct numerical simulation (Fig. 3). The system supports time-periodic patterns containing structures within bumps [Fig. 3(a)]. This pattern is observed as we move away from the Turing bifurcation but stay close to the Hopf curve. Structures of this type, in which the bumps of a Turing pattern are periodically modulated in time, were observed initially in sector IV of Fig. 2(a). Spatiotemporal patterns of this form, with modulation at the core, were found only in parameter sets where the Turing and Hopf codimension-2 point is present, as expected. Structures within bump solutions are not seen in standard neural field models. They are however commonly observed in spiking neuron models [36,37], which emphasises that this next generation neural mass model retains information about the underlying spiking model.

In region IV, we also observe an number of interesting patterns, such as the wandering bump [Fig. 3(b)] and a form of standing wave, where both the width and the height of the bumps is periodically modulated [Fig. 3(c)]. Numerical simulations indicate that the wandering bump is stable for a large area of parameter space and can coexist with a periodic wave train. The standing wave, however, persists for a long time but ultimately is unstable and transitions to a periodic traveling wave (not shown).

**IV. NUMERICAL BIFURCATION ANALYSIS**

To study patterns away from bifurcations, we employ numerical bifurcation techniques, which allows us to compute coherent structures, determine their stability, and track their dependence on control parameters. Here, we employ the numerical tool kit developed by Avitabile [38] and employed in the context of standard neural fields in Refs. [39,40]. This tool kit can be used to compute waves and patterns and their stability. We refer the reader to recent reviews on numerical bifurcation analysis for coherent structures [41,42]. First, we rescaled space such that $x \in [-0.5, 0.5]$, to highlight the dependence on the scale of the domain size $\Lambda$. The equivalent PDE formulation Eqs. (21) and (22)
becomes
\[
\begin{align*}
\partial_t z &= [F(z) + \tilde{G}(z, I)], \\
(\Lambda^2 - \partial_{xx})(1 + \tau_1 \partial_x)^2 g_1 &= \Lambda^2 \kappa_1 f(z), \\
(\Lambda^2 - \partial_{xx}/\beta^2)(1 + \tau_2 \partial_x)^2 g_2 &= \Lambda^2 \kappa_2 f(z).
\end{align*}
\] (32)

We perform numerical bifurcation analysis for heterogeneous spatially patterned steady states and periodic traveling waves of the system above. We construct the stationary patterns by solving for \((z, g_1, g_2)\) the boundary value problem
\[
\begin{align*}
F(z) + \tilde{G}_1(z, g_1) + \tilde{G}_2(z, g_2) &= 0, \\
(\Lambda^2 - \partial_{xx})g_1 - \Lambda^2 \kappa_1 f(z) &= 0, \\
(\Lambda^2 - \partial_{xx}/\beta^2)g_2 - \Lambda^2 \kappa_2 f(z) &= 0.
\end{align*}
\] (33)

with Neumann boundary conditions. Wave trains are solutions to Eq. (32) are found by defining \(\xi = x - ct\) for \(c \in \mathbb{R}\), and setting \(z(x, t) = Z(\xi), g_1(x, t) = G_1(\xi), g_2(x, t) = G_2(\xi)\), where \(Z(\xi), G_1(\xi)\) and \(G_2(\xi)\) are \(\Lambda\)-periodic. To compute wave trains, we solve for \((Z, G_1, G_2, c)\) the boundary value problem
\[
\begin{align*}
\partial_\xi z + (F(Z) + \tilde{G}_1(Z, G_1) + \tilde{G}_2(Z, G_2)) &= 0, \\
(\Lambda^2 - \partial_{\xi\xi})(1 - ct \partial_\xi)^2 G_1 - \Lambda^2 \kappa f(Z) &= 0, \\
(\Lambda^2 - \partial_{\xi\xi}/\beta^2)(1 - ct \partial_\xi)^2 G_2 - \Lambda^2 \kappa f(Z) &= 0, \\
\psi(Z, G_1, G_2) &= 0.
\end{align*}
\] (34)

posed on \(\xi \in [-1/2, 1/2]\) with periodic boundary conditions. The last equation in Eqs. (34) is a standard phase condition [43],
\[
\begin{align*}
\psi(Z, G_1, G_2) &= \int_{-1/2}^{1/2} d\xi \frac{d}{d\xi} \tilde{Z}(\xi)[Z(\xi) - \tilde{Z}(\xi)] \\
&+ \int_{-1/2}^{1/2} d\xi \frac{d}{d\xi} \tilde{G}_1(\xi)[G_1(\xi) - \tilde{G}_1(\xi)] \\
&+ \int_{-1/2}^{1/2} d\xi \frac{d}{d\xi} \tilde{G}_2(\xi)[G_2(\xi) - \tilde{G}_2(\xi)],
\end{align*}
\] (35)

where \((\tilde{Z}, \tilde{G}_1, \tilde{G}_2)\) is a reference template solution, such as one of the solutions obtained via direct simulation. We discretized the differential operators Eqs. (34) using standard differentiation matrices, which are also used to compute linear stability of the coherent structures [38].

### A. Turing patterns

We first analyze the stationary patterns seen in Sec. III, using numerical continuation to verify the analytical results, determine the criticality of the Turing bifurcation, and examine the behavior of these solutions away from the onset of the instability. We continued solutions to the boundary value problem Eq. (33) in the parameter \(\eta_0\) with \(\Lambda = 12\pi\).
FIG. 4. Continuation of spatially periodic patterns. A bifurcation diagram in \( n_0 \) of two stationary patterned states, with different wave numbers. Each branch of patterned states is connected to the branch of homogeneous states via a subcritical Turing bifurcations and reconnect to the steady state within the region of instability. Only the rightmost and left most Turing points correspond to a change in stability of the system. The homogeneous steady state undergoes a Hopf bifurcation at \( n_0 = 3.298 \) as expected from the instability analysis in Sec. III. More interestingly, we also see Hopf bifurcations along the branch of periodic solutions. Solid (dashed) lines represent stable (unstable) solutions. Parameter values: \( v_{\text{syn}} = 15 \), \( \Lambda = 12\pi \); other parameters as described in the caption of Fig. 2(a).

\( v_{\text{syn}} = 15 \), and all other parameters as described in the caption of Fig. 2(a). This corresponds to making a vertical excursion through the two-parameter bifurcation diagram Fig. 2(a). Solving Eqs. (27) and (28) we found two Turing bifurcations at \( n_0 = -0.648, k_c = 0.738 \) and \( n_0 = 12.67, k_c = 0.969 \). Hence, we numerically continued patterns states with \( k = 0.738 \) (blue) and \( k = 0.969 \) (red) (Fig. 4). As expected, the homogeneous steady state bifurcates to patterns at \( n_0 = -0.648 \) (blue) and \( n_0 = 12.67 \) (red), corresponding to the Turing bifurcations found in Sec. III. The stability of the patterned states, as well as the homogeneous state, was numerically calculated along the continuation branch. Along with the Turing bifurcations, the homogeneous steady state undergoes a Hopf bifurcation at \( n_0 = 3.298 \), which matches the value found analytically. The patterned Turing solutions were found to go unstable to a globally oscillating periodic pattern, through a Hopf bifurcation at \( n_0 = 2.8380 \) (blue) and \( n_0 = 5.8546 \) (red). The patterned solutions are also unstable (through a symmetry breaking bifurcation) to broader patterns at low values of \( n_0 \). As anticipated, the bifurcations from the homogeneous steady state are subcritical, hence we have bistability between a spatial pattern and the homogeneous state and the bistability region occurs in a wide region of parameter space. Further numerical continuation results (not shown) indicate that the region of bi-stability increases as the reversal potential \( v_{\text{syn}} \) is increased. As \( v_{\text{syn}} \) decreases toward 0, the static Turing bifurcation points collide, and the patterned states cease to exist, as predicted from the Turing analysis in Sec. III. We found the scenario presented above to be robust to changes in the other parameters.

\[ \begin{align*}
\partial_t \phi &= F(\phi) + \mathcal{G}(\phi, g), \\
(1 - \alpha^2)(1 + \tau \partial_t)^2 \phi &= \kappa f(\phi),
\end{align*} \]

which we pose on \( \xi \in \mathbb{R} \). We now set \( \phi(x, t) = Z(x - ct) \), \( g(x, t) = G(x - ct) \), and we seek traveling fronts as bounded

B. Wave trains

We now shift our focus to wave train solutions originating at a Turing-Hopf bifurcation of the homogeneous steady state. We recall that we find these states as solutions to Eq. (34) with periodic boundary conditions, hence \( \Lambda \) corresponds to the spatial period of the wave train profile. In addition, the phase velocity \( c \) of a wave train is accessible from the boundary-value problem solution.

As in Sec. IV A, the spatial frequency \( k_c \) at bifurcation was found by solving Eqs. (29)–(31), and we continued patterns with this wave number by setting \( \Lambda = 2\pi/k_c \), where \( k_c = 0.739 \) (Figs. 5(a) and 5(b), green curve). We also continued spatial patterns with \( k = 2k_c \) (red curve) and \( k = k_c/2 \) (blue curve), this was achieved by posing the system on domains \( \Lambda = \pi/k_c \) and \( \Lambda = 4\pi/k_c \), respectively. The wave trains bifurcate from the homogeneous steady state with a nonzero phase velocity, at different values of \( n_0 \) [Fig. 5(b)]. The value for which periodic waves emerge for \( \Lambda = 2\pi/k_c \) corresponds to the Turing-Hopf bifurcation (green dot) found in Sec. III, and the speed is equal to \( c = k_c/\Lambda \). The wave trains are unstable for low values of \( n_0 \). For the smaller domain size they are unstable to the stable steady state, whereas for the larger domain size they transition to finer patterns, with a smaller spatial wavelength \( k \).

To fully explore the relationship between the wave speed and the spatial period, we fix the value of \( n_0 = 0 \) and use \( \Lambda \) as a continuation parameter. This opens up the possibility to trace branches of solutions in the \( (c, \Lambda) \) plane, and hence, approximate the dispersion curve of the waves [Fig. 5(c)]. We found that wave trains occur in isolas, and therefore only exist for a finite range of spatial periods. For \( 5.2 < \Lambda < 13.1 \), a fast (stable) wave train coexist with slower (unstable) one. Whereas, when \( 3.2 < \Lambda < 5.2 \) and \( 13.1 < \Lambda < 28.0 \) the two waves are unstable. For all other values of \( \Lambda \) we do not see wave train solutions. If \( n_0 \) is increased, the dispersion curve is no longer an isola, but rather a monotonically increasing function. Thus, in this regime, the system supports periodic traveling waves for all values of the spatial period, above a threshold value.

C. Fronts

Standard neural field models are known to support traveling fronts (for exponentially decaying kernels), which are travelling waves whose profile connects a uniform high-activity state to another low-activity state [44,45]. It is therefore natural to search for these coherent structures in our new neural field model Eqs. (19) and (20). As in any other nonlocal neural field, the existence of the high- and low-activity states depends on the choice of the synaptic kernel. As inhibition is not necessary for the generation of localized patterns, such as traveling fronts, in this section we consider only a single synaptic conductance, \( m = 1 \) and suppress the \( m \) label, leading to the equivalent PDE formulation

\[ \begin{align*}
\partial_t z &= F(z) + \mathcal{G}(z, g), \\
(1 - \alpha^2)(1 + \tau \partial_t)^2 z &= \kappa f(z),
\end{align*} \]
solutions $U(\xi) = [U_1(\xi), \ldots, U_6(\xi)]$ to the boundary-value problem

$$\partial_\xi U = \mathcal{N}(U), \quad \xi \in \mathbb{R}, \quad \lim_{\xi \to \pm \infty} U(\xi) = U^\pm,$$

where $\mathcal{N}: \mathbb{R}^6 \to \mathbb{R}^6$ is the real-valued nonlinear function

$$\mathcal{N}(U) = \begin{pmatrix}
- \text{Re}[F(U_1 + iU_2) + G(U_1 + iU_2, U_3)]/c \\
- \text{Im}[F(U_1 + iU_2) + G(U_1 + iU_2, U_3)]/c \\
(U_3 - U_4)/(\tau c) \\
U_5 \\
U_6 \\
U_3 + [U_6 + \kappa f(U_1 + iU_2) - U_4]/(\tau c)
\end{pmatrix}.$$

In this spatial-dynamical system formulation of the problem, the first three components of $U$ have a direct interpretation in terms of the state variables $(z, g)$ of Eq. (36),

$$U_1 = A \equiv \text{Re} Z, \quad U_2 = B \equiv \text{Im} Z, \quad U_3 = G,$$

whereas $U_4$, $U_5$, and $U_6$ are auxiliary variables, necessary to cast the problem as a system of first-order differential equations in $\xi$. The equilibria $U^\pm = (U_1^\pm, U_2^\pm, U_3^\pm, U_4^\pm, U_5^\pm, U_6^\pm)$ of the spatial-dynamical system Eq. (37) correspond to high- and low-activity homogeneous steady states of Eq. (36) and are completely determined by solving for $(U_1, U_2, U_3)$ the algebraic problem

$$\text{Re}[F(U_1 + iU_2) + G(U_1 + iU_2, U_3)] = 0,$$

$$\text{Im}[F(U_1 + iU_2) + G(U_1 + iU_2, U_3)] = 0,$$

$$\kappa f(U_1 + iU_2) - U_3 = 0.$$  \hspace{1cm} (38)

We define $U^+$ as the high activity state, which displays high synaptic conductance and $U^-$ as the low activity state, displaying lower synaptic conductance. Note that we also seek the symmetric counterpart solution where $\lim_{\xi \to \pm \infty} U(\xi) = U^\pm$. We have continued solutions to Eq. (38) in $\eta_0$ and $v_{syn}$ using XPPAUT [35] [Fig. 6(a)]. The system has three fixed points in the region enclosed by the saddle-node curves, two of which are stable ($U^\pm$). Therefore, we look for traveling waves in this shaded region of parameter space. We note that, as $\tau$ is decreased, a Hopf bifurcation of the $U^-$ state arises, opening up the possibility of creating heteroclinic connections to periodic orbits, which we will not consider further here.

The state at $\xi \to - \infty$ ($\xi \to \infty$) displays a high-conductance (low-conductance) $G$, hence a high (low) firing, and it is therefore referred to as the high (low) activity state [Fig. 6(b)]. We computed traveling waves using the routines from Ref. [38], which allows us to study the spectral stability of the waves. Computations are performed on a large truncated domain $\Lambda = 60$, and plotted on $[-10, 10]$ for convenience. Interestingly, we see ripples in the wake of the front, which indicates that the solution connects a node to a focus. The solution in the phase space $(A, B, G)$ illustrates that the high-activity state ($U^-$) is a focus, and the low activity one ($U^+$) a node.
FIG. 6. Numerical continuation results for traveling fronts. (a) Two-parameter bifurcation diagram of stationary homogeneous states of Eq. (36) [equilibria of Eq. (37)] in the \((\eta_0, v_{syn})\) plane. We plot the locus of saddle-node bifurcations of the steady state, colliding at a cusp bifurcation. To the left of the cusp we identify a low-activity state, \(U^-\), and a high-activity one, \(U^+\), which coexist and are stable in the shaded area. Parameter values: \(\Delta = 0.5\), \(\kappa = 5\), \(\tau = 1\). (b) Travelling front profile, computed by solving Eq. (37) on a truncated domain \([-30, 30]\), for \(\eta_0 = -3\), \(v_{syn} = 4\). We show the profiles in the synaptic conductance variable \(G_\xi\) and the synchrony variable \(R(\xi) = |Z_\xi(\xi)|\). (c) The travelling front in (b) is a heteroclinic orbit connecting the equilibria \(U^+\) and \(U^-\) of the spatial-dynamical system Eq. (37). We show a projection of the (approximate) heteroclinic orbit in the \((A, B, G)\) space. (d) Numerical continuation of the travelling front \(U(\xi)\) found in (b) (blue) and its symmetric counterpart \(U(-\xi)\) (red), using \(\eta_0\) as continuation parameter and \(c\) as solution measure. The fronts live on an isolated branch and destabilise at saddle-node bifurcations. The bifurcation curve is symmetric, with respect to the axis \(c = 0\). Solutions with \(c > 0\) and \(c < 0\) are related via the transformation \(U(\xi) \leftrightarrow U(-\xi)\).

We continued the traveling wave shown in Fig. 6(b) (blue), and its symmetric counterpart (red), in the mean background drive \(\eta_0\), using \(c\) as a solution measure [Fig. 6(d)]. Fronts live on an isolated branch and destabilise at saddle-node bifurcations. The bifurcation diagram is symmetric with respect to the axis \(c = 0\), as solutions on the branch with \(c > 0\) and \(c < 0\) are related via the transformation \(U(\xi) \leftrightarrow U(-\xi)\). Up to six coexisting waves exist in a wide region of \(\eta_0\) parameter space, albeit only two of them are stable. In addition, we found stable waves in which the high activity state \(U^+\) is moving across the tissue, invading the low activity state \(U^-\), and vice versa. The inversion of velocity occurs where the blue and red stable branches overlap.

As the isola of traveling fronts is traced, these solutions gain or lose oscillations in the wake of the wave. To investigate further this aspect, we monitor the spectrum of \(U^\pm\) [as equilibria of the spatial-dynamical system Eq. (37)] as we move along the branch. Taking a vertical excursion in Fig. 6(d), we find three independent solutions, one of which is stable and two of which are unstable. We examine the stability of the fixed points \(U^\pm\) in the traveling wave frame for each of these solutions. As expected, oscillations in the wake of the wave are absent where the unstable spectrum of \(U^-\) is purely real [Fig. 7(a)], and they develop when a complex-conjugate pair of eigenvalues crosses the imaginary axis [Fig. 7(b)]. We also find that the amplitude of the oscillations is small when the real part of the complex eigenpair is small [Fig. 7(c)].

V. DISCUSSION

We have presented the derivation of an atypical neural field model from a network of spatially distributed \(\theta\)-neurons. In the reduced model, which we dub a next generation neural field model, within population synchrony drives the population firing rate. This model supports a range of patterns, such as bumps, waves and breathers. Noteworthy is the state characterized by structures within bumps, as these states are not seen in standard neural mass models. These structures instead typify patterns seen in networks of spiking neurons [36,37], which signifies that by maintaining the notion of within population synchrony this neural field model can retain information about the underlying spiking network. Exotic states, with within-bump oscillations, were found in the region where the Hopf and Turing bifurcations collided.

A Turing instability analysis provided us with an understanding of how the system behaved close to bifurcation points, allowing us to determine when the system transitioned from the homogeneous steady state. However, unlike the Amari model we cannot use the Heaviside approximation to make further analytical progress since the firing rate is now a fixed real valued function of the Kuramoto order parameter. As such, we have moved to numerical continuation techniques to analyze the behavior of the system away from these bifurcation points. Numerical techniques were also used to examine the existence and stability of travelling fronts.

Previous work [25] illustrated that the point version of this model could support \(\beta\)-rebound, an event-related modulation of the \(\beta\) rhythm, as seen in MEG. This work showed that an external-time-dependent drive desynchronized the population and when switched off the population synchrony peaked before returning back to its steady-state level. These changes in population synchrony resulted in modulation of the \(\beta\) rhythm, similar to modulations observed in neuroimaging data. An interesting extension of this work would be to include a similar spatially dependent drive in the neural field model presented here and examine how the inclusion of space affects \(\beta\)-band modulations, and perhaps explain why \(\beta\) rebound is seen in both hemispheres during movement of a single side of the body. More generally, the model parameters can be altered so that the population oscillates at other frequencies, and hence, used to explain other event-related desynchronization and synchronization phenomena in the brain.

In Sec. IV, we pointed to the existence of a front which connects periodic orbits to nodes and focuses, for the model with an exponential coupling kernel. We observed such fronts by decreasing the synaptic time constant \(\tau\) (Fig. 8). The
FIG. 7. Spectrum of the high- and low-activity homogeneous states connected by selected traveling wave profiles, in Fig. 6. (a) \( c = -0.8769 \), (b) \( c = 0.3594 \), (c) \( c = 0.9470 \). Parameter values: \( \eta_0 = -3 \), \( v_{\text{syn}} = 4 \), \( \Delta = 0.5 \), \( \kappa = 5 \), \( \tau = 1 \).

The numerical machinery used here does not allow for the continuation of these solutions, known as defects. The analysis of defects is still an open problem. Close examination of Fig. 8 reveals that there are two fronts in the connection between the node and the limit cycle, which appear to be moving at different speeds. Even more interesting, would be the analysis of fronts which connect two periodic orbits of different amplitudes. The spreading of such a wave across the cortex could be viewed as the spreading of an epileptic seizure. Another numerical challenge would be to continue the exotic patterned states seen in Sec. III when the Turing and Hopf bifurcations collide. These patterns have both a spatial and a temporal period, which would require extending the numerical machinery [38] to continue both a spatial and a temporal pattern. This has been achieved in Ref. [46] for the Brusselator model.

A natural extension to the work presented in Secs. III and IV would be to include a second spatial dimension. It is more natural to view the cortex as a two dimensional sheet and examine the propagation of waves across it. We would expect that the 2D system supports the two dimensional versions of the patterned states presented here, but also potentially some more exotic states. Extending both the Turing analysis and the numerical machinery to include a second spatial extension is worthy of further exploration.

ACKNOWLEDGMENTS

D.A. was supported by the Engineering and Physical Sciences Research Council under Grant No. EP/P510993/1. S.C. was supported by the European Commission through the FP7 Marie Curie Initial Training Network 289146, NETT: Neural Engineering Transformative Technologies.

APPENDIX A: JACOBIAN

To calculate the Jacobian we first write the system Eqs. (19) and (20) in full six-dimensional form,

\[
\frac{\partial a}{\partial t} = b (a - 1) - b (a + 1) (\eta_0 + v_{\text{syn}} s_1 + v_{\text{syn}}^2 s_2) - (a + 1) \Delta - \frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2),
\]

where

\[
\begin{align*}
\frac{\partial b}{\partial t} &= -\frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2), \\
\frac{\partial s_1}{\partial t} &= \frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2), \\
\frac{\partial s_2}{\partial t} &= \frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2), \\
\frac{\partial g_1}{\partial t} &= \frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2), \\
\frac{\partial g_2}{\partial t} &= \frac{1}{2} (a^2 - b^2 - 1)(\Delta + g_1 + g_2).
\end{align*}
\]
\[
\frac{\partial b}{\partial t} = -\frac{1}{2}[\Delta - b\Delta - ab(\Delta + g_1 + g_2)] + \frac{1}{2}[(a + 1)^2 - b^2](\eta_0 + v_{1}\psi g_1 + v_{2}\psi g_2),
\]
\[
\frac{\partial g_1}{\partial t} = \frac{1}{\tau_1}(-g_1 + K_1),
\]
\[
\frac{\partial K_1}{\partial t} = \frac{1}{\tau_1}[-K_1 + \kappa_1 w_m \otimes f(a + ib)],
\]
\[
\frac{\partial g_2}{\partial t} = \frac{1}{\tau_2}(-g_2 + K_2),
\]
\[
\frac{\partial K_2}{\partial t} = \frac{1}{\tau_2}[K_2 - \kappa_2 w_m \otimes f(a + ib)].
\]

The Jacobian of the system can be written as follows:
\[
\mathcal{J}(k) = \begin{pmatrix}
\mathcal{J}_{11} & \mathcal{J}_{12} \\
\mathcal{J}_{21}(k) & \mathcal{J}_{22}
\end{pmatrix},
\]
where
\[
\mathcal{J}_{11} = \begin{pmatrix}
\frac{\partial}{\partial a} & \frac{\partial}{\partial b} & \frac{\partial}{\partial g_1} & \frac{\partial}{\partial g_2} & \frac{\partial}{\partial K_1} & \frac{\partial}{\partial K_2}
\end{pmatrix},
\]
\[
\mathcal{J}_{12} = \begin{pmatrix}
0 & 0 & 0 & 0 & 0 & 0
\end{pmatrix},
\]
\[
\mathcal{J}_{21}(k) = \begin{pmatrix}
\tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial a} & \tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial b} & \tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial g_1} & \tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial g_2} & \tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial K_1} & \tau_1^{-1} \kappa_1 \hat{w}_1 \frac{\partial f}{\partial K_2}
\end{pmatrix},
\]
\[
\mathcal{J}_{22} = \begin{pmatrix}
-\tau_1^{-1} & 0 & 0 & 0 & 0 & 0 \\
-\tau_1^{-1} & 0 & 0 & 0 & 0 & 0 \\
0 & \tau_1^{-1} & 0 & 0 & 0 & 0 \\
0 & 0 & \tau_1^{-1} & 0 & 0 & 0 \\
0 & 0 & 0 & \tau_1^{-1} & 0 & 0 \\
0 & 0 & 0 & 0 & \tau_1^{-1} & 0
\end{pmatrix},
\]

The variables, \(a, b, g_1,\) and \(g_2\) are evaluated at the steady state and hence depend upon the control parameters, \(\hat{w}_i\) depend on \(k\) and \(\beta\) and \(f\) is given by Eq. (17).

The derivatives are computed as follows:
\[
\frac{\partial}{\partial a} \left( \frac{\partial a}{\partial t} \right) = \frac{\partial}{\partial b} \left( \frac{\partial b}{\partial t} \right) = -b - (a + 1)\Delta - b(\eta_0 + v_{1}\psi g_1 + v_{2}\psi g_2) - a(g_1 + g_2).
\]

\[
\frac{\partial}{\partial a} \left( \frac{\partial a}{\partial t} \right) = \frac{\partial}{\partial b} \left( \frac{\partial b}{\partial t} \right) = (a - 1)(a + 1)(\eta_0 + v_{1}\psi g_1 + v_{2}\psi g_2) + b(\Delta + g_1 + g_2).
\]

\[\text{APPENDIX B: TURING COEFFICIENTS}\]

The coefficients of the characteristic Eq. (23) in Sec. III are calculated as follows:
\[
p_0 = \frac{(A^2 + B^2)/(\tau_1 \tau_2)^2},
\]
\[
p_1 = 2[(\tau_1 + \tau_2)^2(A^2 + B^2) - A]/(\tau_1 \tau_2)^2,
\]
\[
p_2 = \left[(\tau_1^2 + \tau_2^2 + 4\tau_1 \tau_2)(A^2 + B^2) + 1 - 4(\tau_1 + \tau_2)A\right]/(\tau_1 \tau_2)^2,
\]
\[
p_3 = 2\left[(\tau_1 \tau_2^2 + \tau_1^2 \tau_2)(A^2 + B^2) + (\tau_1 + \tau_2 - 4A)ight.
\]
\[\left.- (\tau_1^2 + \tau_2^2)A\right]/(\tau_1 \tau_2)^2,
\]
\[
p_4 = \tau_1^{-2} + \tau_2^{-2} + A^2 + B^2 + 4(1 - (\tau_1 + \tau_2)A)/(\tau_1 \tau_2),
\]
\[
p_5 = 2(\tau_1^{-1} + \tau_2^{-1} - A),
\]
\[
q_0 = \kappa_i C_i / (\tau_i j)^2,
\]
\[
q_1 = \left[\kappa_i f(\tau_1, \tau_2) + 2\tau_j \kappa_i C_i\right] / (\tau_i \tau_j)^2,
\]
\[
q_2 = \left[2\kappa_i f(\tau_1, \tau_2) + \tau_i \kappa_i C_i\right] / (\tau_i^2 \tau_j),
\]
\[
q_3 = \kappa_i f(\tau_1, \tau_2) / \tau_j^2,
\]
where \(i, j \in \{1, 2\}\)

\[
A = \frac{\partial}{\partial a} \left( \frac{\partial a}{\partial t} \right) = \frac{\partial}{\partial b} \left( \frac{\partial b}{\partial t} \right) = \frac{\partial}{\partial a} \left( \frac{\partial b}{\partial t} \right) - \frac{\partial}{\partial b} \left( \frac{\partial a}{\partial t} \right)
\]
\[
B = \frac{\partial}{\partial b} \left( \frac{\partial a}{\partial t} \right) = \frac{\partial}{\partial a} \left( \frac{\partial b}{\partial t} \right)
\]
\[
C_i = -Af(\tau_1, \tau_2) + \frac{B}{\pi} \left[2h \left(1 + \frac{2b}{(1 + a)^2 + b^2}\right)\right].
\]

[1] D. M. Alexander, C. Trengove, and C. van Leeuwen, Cogn. Process. 16, 365 (2015).
[2] D. Golomb and Y. Amitai, J. Neurophysiol. 78, 1199 (1997).
[3] P. L. Nunez and R. Srinivasan, Clin. Neurophysiol. 117, 2424 (2006).
[4] M. Massimini, J. Neurosci. 24, 6862 (2004).
[5] H. Berger, Archiv für Psychiatrie und Nervenkrankheiten 87, 527 (1929).
[6] K. Wimmer, D. Q. Nykamp, C. Constantinidis, and A. Compte, Nat. Neurosci. 17, 431 (2014).
[7] K. Zhang, J. Neurosci. **16**, 2112 (1996).
[8] C. R. Laing and C. C. Chow, J. Comput. Neurosci. **12**, 39 (2002).
[9] P. C. Bressloff and M. A. Webber, J. Comput. Neurosci. **32**, 233 (2012).
[10] R. Ben-Yishai, R. L. Bar-Or, and H. Sompolinsky, Proc. Natl. Acad. Sci. USA **92**, 3844 (1995).
[11] S. Coombes, P. P. Beim Graben, R. Potthast, and J. Wright, *Neural Fields: Theory and Applications* (Springer, Berlin, 2014), p. 487.
[12] R. L. Beurle, Philos. Trans. R. Soc. London B **240**, 55 (1956).
[13] H. R. Wilson and J. D. Cowan, Biophys. J. **12**, 1 (1972).
[14] H. R. Wilson and J. D. Cowan, Biol. Cybern. **13**, 55 (1973).
[15] S. Amari, Biol. Cybern. **17**, 211 (1975).
[16] S. Amari, Biol. Cybern. **27**, 77 (1977).
[17] S. Coombes, Biol. Cybern. **93**, 91 (2005).
[18] P. C. Bressloff and S. Coombes, Cogn. Comput. **5**, 281 (2013).
[19] P. L. Nunez and R. Srinivasan, *Electric Fields of the Brain: The Neurophysiology of EEG*, 2nd ed. (Oxford University Press, Oxford, 2005).
[20] F. L. da Silva and A. V. Rotterdam, in *Electroencephalography: Basic Principles, Clinical Applications and Related Fields*, edited by E. Niedermeyer and F. L. da Silva (Lippincott Williams & Wilkins, Philadelphia, 2005), pp. 107–126.
[21] G. Pfurtscheller and F. H. L. da Silva, Clin. Neurophysiol. **110**, 1842 (1999).
[22] T. B. Luke, E. Barreto, and P. So, Neural Comput. **25**, 3207 (2013).
[23] E. Montbrió, D. Pazó, and A. Roxin, Phys. Rev. X **5**, 021028 (2015).
[24] C. R. Laing, J. Appl. Dynam. Syst. **14**, 1899 (2015).
[25] A. Byrne, M. J. Brookes, and S. Coombes, J. Comput. Neurosci. **43**, 143 (2017).
[26] S. Coombes and A. Byrne, in *Lecture Notes Nonlinear Dynamics in Computational Neuroscience: from Physics and Biology to ICT*, PoliTO, edited by A. Torcini and F. Corinto (Springer, Berlin, 2019), pp. 1–16.
[27] J. M. Esnaola-Acebes, A. Roxin, D. Avitabile, and E. Montbrió, Phys. Rev. E **96**, 052407 (2017).
[28] G. B. Ermentrout and J. D. Cowan, Biol. Cybern. **34**, 137 (1979).
[29] P. C. Bressloff, J. D. Cowan, M. Golubitsky, P. J. Thomas, and M. C. Wiener, Philos. Trans. R. Soc. London B **356**, 299 (2001).
[30] S. Coombes, NeuroImage **52**, 731 (2010).
[31] F. Gabbiani and S. Cox, *Mathematics for Neuroscientists* (Elsevier Academic Press, Cambridge, MA, 2010).
[32] G. B. Ermentrout and N. Kopell, SIAM J. Appl. Math. **46**, 233 (1986).
[33] E. Ott and T. M. Antonsen, Chaos **18**, 037113 (2008).
[34] S. Coombes, G. Lord, and M. Owen, Physica D **178**, 219 (2003).
[35] G. B. Ermentrout, *Simulating, Analyzing, and Animating Dynamical Systems: A Guide to XPPAUT for Researchers and Students* (SIAM Books, Philadelphia, PA, 2002).
[36] C. Laing and C. C. Chow, Neural Comput. **13**, 1473 (2001).
[37] C. C. Chow and S. Coombes, SIAM J. Appl. Dynam. Syst. **5**, 502 (2006).
[38] D. Avitabile, in *Proceedings of the 2nd International Conference on Mathematical Neuroscience* (Juan-les-Pins, 2016).
[39] J. Rankin, D. Avitabile, J. Baladron, G. Faye, and D. J. B. Lloyd, SIAM J. Sci. Comput. **36**, B70 (2014).
[40] D. Avitabile and H. Schmidt, Physica D **294**, 24 (2015).
[41] C. R. Laing, J. Math. Neurosci. **4**, 13 (2014).
[42] A. R. Champneys and B. Sandstede, in *Numerical Continuation Methods for Dynamical Systems: Path Following and Boundary Value Problems*, edited by B. Krauskopf, H. M. Osinga, and J. Galán-Vioque (Springer, Berlin, 2007), pp. 331–358.
[43] E. J. Doedel, Congr. Numer. **30**, 265 (1981).
[44] B. Ermentrout, Rep. Prog. Phys. **61**, 353 (1998).
[45] P. C. Bressloff, J. Phys. A: Math. Theor. **45**, 033001 (2012).
[46] D. Avitabile, Computation of Planar Patterns and Their Stability, Ph.D. thesis, University of Surrey (2008).