Associations between high intensity zones, Modic and endplate changes in lumbar spine of low back pain patients

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Kerstin Lagerstrand  kerstin.lagerstrand@vgregion.se
Goteborgs universitet Institutionen for kliniska vetenskaper
Corresponding Author

Helena Brisby
Goteborgs universitet Institutionen for kliniska vetenskaper

Hanna Hebelka
Goteborgs universitet Institutionen for kliniska vetenskaper

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Abstract

Background High intensity zones (HIZ), Modic and endplate changes have all been pointed out as potential markers of low back pain (LBP). If an association between these morphological features exist, it may not only deepen the understanding of the underlying patho-physiological mechanism of LBP but may also improve the diagnostics by enabling stratification between individuals with non-specific LBP as well as within individuals having multi-segmental changes. The aim was to investigate if HIZ, Modic and endplate changes are associated and if endplate and vertebral T2-values reflect functional tissue characteristics related to these morphological features.

Methods 150 IVDs with corresponding endplates and vertebrae in 26 chronic LBP-patients (25-69y, mean 38y, 11 males) were examined with T1- and T2-weighted MRI, and T2-mapping. Associations between morphological features and between morphological features and functional T2-values were determined.

Results HIZ (62% of patients, 1-2/patient) was associated with endplate changes (100% of patients, 1-7/patient) (p=0.0003 and 0.0004 for upper and lower endplates), with an occurrence of 91% for upper and 71% for lower endplates adjacent to discs with HIZ. Modic changes (81% of patients, 1-3/patient) was associated with endplate changes (p<0.0001) with an occurrence of 87% for endplates adjacent to vertebrae with Modic changes. The occurrence of both HIZ and Modic changes was 43% (p=0.0001) for upper and 29% (p=0.003) for lower vertebrae. Significantly higher T2-values (p<0.004) were found in the vertebral tissue with associated Modic changes and HIZ.

Conclusions This study of LBP-patients suggests that HIZ is associated with simultaneous presence of both Modic and endplate changes in the same motion segment. If these three simultaneous morphological features are linked to an active inflammatory process, reflected as a clinical specific pain profile remains to be investigated.
Background

Low back pain (LBP) is the most costly non-communicable endemic disease worldwide (1). The condition is multifactorial and in addition to central nervous system adaptations and responses, damage to the non-nervous spinal tissues is a key component. High intensity zones (HIZ), Modic changes (MCs) and endplate (EP) changes are known to be a part of the degenerative cascade and have been suggested to be associated with LBP (2, 3). However, the association between such changes and LBP is not fully elucidated. Neither is their relationship with each other. In the search for reliable LBP-markers, better diagnostic tools are warranted (4, 5). The combination of HIZs, MCs and EP-changes could potentially be a stronger indicator of painful spine segments than the presence of these individual features alone. If such association exist, it may not only deepen the understanding of the underlying patho-physiological mechanism of LBP but may also enable stratification between individuals with non-specific LBP as well as within individuals having multi-segmental changes and thereby improve the diagnostics and clinical decision making. It has been suggested that HIZ is an effect of annular tears with accumulation of substances that are toxic to the disc cells and surrounding structures and linked with inflammation and degenerative changes (6, 7). Moreover, MC Type I, is likely of inflammatory origin, and associated with disruption and fissuring of the EPs (8, 9). Further, increased levels of pro-inflammatory mediators have been detected in the EP itself with adjacent subchondral bone edema (MC type I) when compared to EPs from vertebral fracture patients (10). Hence, such biochemical changes may compromise the function of the IVD, EP and vertebrae and play a crucial role in the development of LBP (11).

With the implementation of functional magnetic resonance imaging (MRI) methods, detection of early biochemical changes of the IVD, EP and vertebrae is feasible (12).
Recent work has shown that in the presence of HIZs, altered IVD T2-values are detected at the position of the nucleus pulposus (13, 14). Even scarce in numbers, some T2-mapping studies have demonstrated subtle deterioration of the biochemical composition of the EPs (15, 16). Moreover, the feasibility of T2-mapping for objective characterization of the EPs and vertebrae has recently been demonstrated (17). This together with the fact that T2-mapping provide supplemental information about the tissue matrix and reflect presence of edema, makes the method a potential tool for monitoring of tissue changes linked to function. Finally, functional properties of the EPs may also be displayed using T2-mapping in combination with axial loading during MRI (aMRI) as compared to conventional imaging, when the spine is unloaded (uMRI) (17).

The aim of the study was firstly to investigate if HIZ, Modic and EP-changes are associated with each other and secondly to investigate if EP and vertebral T2-values reflecting functional tissue characteristics were related to these MRI findings.

Methods

Study-cohort

Twenty-six patients with chronic LBP (25-69y, mean 38y, 11 males), referred to the radiology department with non-specific LBP, were consecutively included. Inclusion criteria were severe LBP without radiating pain for more than 6 months, clinically severe enough to be considered for surgery, without signs of nerve root compromise during clinical examination, and age between 20-70 years. Exclusion criteria were previous spine surgery and contraindications for MRI.

MRI

The IVDs, EPs and vertebrae were examined (from superior EP L1 to vertebra S1) using a 1.5 T scanner (Magnetom Aera, Siemens Erlangen, Germany) with both the posterior and anterior phased array coil applied for increased signal-to-noise-ratio.
Standardized sagittal T1 weighted (T1W) MRI (320x320 matrix, slice thickness: 3.5 mm, slice gap [SLG]: 0.7 mm, field of view [FOV]: 300x300 mm², number of excitations [NEX]: 2) and standardized sagittal T2W-MRI (384x384 matrix, SLT: 3.5 mm, SLG: 0.7 mm, FOV 300x300 mm², NEX: 1), and axial T2W-MRI (256x256 matrix, SLT: 3.5 mm, SLG: 0.7 mm, FOV: 220x220 mm², NEX: 1) were performed. Additionally, all subjects were scanned with quantitative T2-mapping (256x256 matrix, SLT: 3.5 mm, SLG: 0.7 mm, FOV: 220x220 mm², NEX: 1). The T2-mapping of the spine was performed in the sagittal view covering L1- S1. The participants were examined twice with the present protocol, initially with uMRI and subsequently with aMRI. T2-mapping was performed at the end of the protocol, approximately 20 minutes after the first measurement. Hence, the spine had been loaded for 20 minutes before T2-mapping.

The aMRI measurements were performed with a DynaWell compression device (DynaWell diagnostics AB, Las Vegas, NV, USA) with load, corresponding to 50% of the body weight.

**Post-processing if the MR images**

All post processing of the images was performed with the dedicated analysis tool of the scanner (Syngio Via, Siemens Erlangen, Germany).

The conventional T1W- and T2W-images were used for classification of IVD degeneration into Pfirrmann grade according to recommendations (18). The grading was performed by a senior radiologist (15 years of experience) and was based on the uMRI examinations using all images in the image stack.

Conventional images were also used for identification of HIZs, MCs and EP-changes (Figure 1), where the MCs were classified into MC Type I, II and II according to Modic et al. (19). HIZs was defined as the presence of a high signal located in the posterior annulus fibrosus, visible only on the T2W- but not on the T1W-images (20). EP-change was defined
as apparent visual inhomogeneity and discontinuity in signal in the EP-zone (Figure 1), identified in the conventional MR images and restricted to the EP. EPs with Schmorl’s nodules were not included. Identification of the morphological features was performed by the senior radiologist.

Associations between HIZs, MCs and EP-changes within the same motion segment were determined. To determine associations for superior and inferior EPs separately, the vertebrae were divided horizontally into two equally large parts, hereafter called superior and inferior vertebrae.

Functional behaviors of the EPs and vertebrae in terms of T2 were retrieved from T2-maps acquired both with uMRI and aMRI. The T2-maps were reconstructed from optimized fitting of the raw data and then reformatted into 10 mm non-overlapping slices, where the three central slices were used in the estimation, thus, covering 30 mm of the EP and vertebral width. For determination of EP T2-values, the T2-maps were manually segmented into regions of interest (ROIs) covering the EP-zone (17). In general, the EP ROI was positioned approximately one pixel away from the visible edge of the IVD and vertebral body. With this strategy, the EP-zone was assumed to include both bony and cartilage EP. The median T2-value within the ROI was calculated and used as a measure of the EP T2-value. Similarly, the vertebral T2-value was determined in the superior and inferior vertebrae as the median value within these regions. All segmentations were performed by a trained observer, supervised by a senior radiologist with 20 years of experience. The intra- and interobserver ICC for the vertebral T2-value were excellent (0.9–1.0), for the superior EPs: fair to good (0.5–0.6) and for the inferior EPs: good to excellent (0.6–0.8).

Statistics

All statistical analyses were performed using SAS Software version 9.4 (SAS Institute Inc., Cary, NC).
For comparison between groups and differences within groups, a mixed linear model adjusted for multiple observations within subjects was used. The comparisons were performed with correction for Pfirrmann grades. Results are presented as adjusted means (with 95% confidence intervals) together with p-values. All tests were two-tailed at 0.05 significance level. To test difference in variances between groups, the two-tailed F-test was used at 0.05 significance level.

Inter-rater agreement for the T2-measurements was displayed using intraclass correlation coefficients (ICC) with 95% confidence intervals. ICC model 2 was used with single measurement to determine consistency in agreement. ICC-values <0.4 represent poor agreement, 0.4-0.75 represent fair to good agreement and >0.75 indicate excellent reliability.

Results

HIZs were found in 16% of the IVDs (in 62% of the patients, 1-2/patient) and EP-changes were found in 39% of the EPs (100% of the patients, 1-7/patients). Corresponding values for MC of any type and MC Type I were 13% (81% of the patients, 1-3/patient)) and 5% (27% of the patients, 1-3/patient).

The patient cohort displayed the following Pfirrmann grade distribution, Pfirrmann 1-5: 8, 50, 29, 13, 0%

Associations between HIZ, MC and EP-changes

Associations between the investigated morphological features are presented in Table 1. The presence of HIZ was associated with the presence of EP-changes (p=0.0003 and 0.0004 for superior and inferior EPs, respectively), with an occurrence of 91% for superior and 71% for inferior EPs adjacent to IVDs with HIZ. Also, presence of MC of any type was associated with presence of EP-changes (p<0.0001) with an occurrence of 87% for EPs.
adjacent to vertebrae with MCs. Finally, the occurrence of both HIZ and MC in the same segment was 43% (p=0.0001) for superior and 29% (p=0.003) for inferior vertebrae. The association between MC Type I findings and HIZ and EP-changes are not presented due to limitation in power.

**Vertebral T2-values**

Associations were found between the vertebral T2-value (at uMRI) and the investigated morphological features. The T2-value was significantly higher for vertebrae with presence of HIZ in adjacent IVDs in comparison with no HIZ (103±11 vs 99±9, p=0.001). This was also true for superior (102±11 vs 99±9, p=0.001) and inferior vertebrae (106±12 vs 100±9; p=0.0003). As expected, the vertebral T2-value was found to be significantly higher for presence of MC compared to no MC (all: 104±11 vs 98±11ms, p=0.003; superior: 101±11 vs 97±11ms, p=0.03; inferior: 101±11 vs 99±12ms, p=0.001), and for MC Type I compared to no MC Type I (all: 104±11 vs 98±11ms; p=0.003; superior: 101±11 vs 97±11ms, p=0.04; inferior: 111±11 vs 99±12ms, p=0.001). The vertebral T2-value was not associated with EP-changes (p>0.6).

Also for alMRI-uMRI, the investigated morphological features were not found to be associated with the vertebral T2-value (p>0.5).

**EP T2-values**

Regardless of type of morphological changes in the segment, similar EP T2-values (at uMRI) were detected (38±15, 39±15, 37±15, 35±10, and 34±9ms for no morphological change, EP-change, HIZ, MC any type, and MC Type I; p>0.1).

However, the effect of alMRI on the EP T2-value varied depending on type of morphological changes in the segment. For EPs with no morphological changes in the EPs or in the adjacent vertebra, nor any adjacent HIZ, a large spread in the T2-value was seen for alMRI-uMRI (SD=12ms). A narrower T2-distribution was statistically verified for EPs
with MC any type and MC Type I (6 and 5 ms: p < 0.001), but not for HIZ and EP-changes (11 and 8 ms: p > 0.07).

Discussion

This study shows that the presence of HIZ is associated with MCs. Furthermore, HIZ was found to be associated with EP-changes, which in turn were found to be associated with MCs. Hence, simultaneous presence of these morphological features in the same motion segment was a common characteristic in this LBP cohort, supporting previous observations with crosstalk between inflammatory IVD and vertebral changes (21). Moreover, T2-mapping was found to objectively reflect EP and vertebral tissue changes associated with HIZs and MCs. The significantly higher vertebral T2-value for MC Type I and/or with HIZ in adjacent IVDs may be a reflection of a general inflammatory state, since higher T2-values, at least partly, reflect the higher content of water molecules and MC Type I is believed to display edema (9).

MC is a common phenomenon for spinal degenerative diseases, but it is not fully elucidated what mechanisms leads to MCs. Abnormal load and stress are hypothesized to affect the EPs and the microenvironment of the adjacent vertebrae, resulting in histological changes that exhibit signal changes on MR images, i.e. MCs. Another hypothesis is that MCs result from an inflammatory reaction by toxic substances from the IVD (22). Also HIZ is assumed to have an inflammatory component originating from proinflammatory substances appearing in the annular tears (6, 23). Crock et al. (24) found that upregulation of inflammatory mediators within the IVD could result in local inflammation in the EPs and vertebrae associated with LBP. This finding was confirmed by Rannou et al. (25). Moreover, Ohtori et al. (26) argued that inflammatory mediators and
nerve ingrowth into the EPs might be a cause of LBP, and that MC Type I more likely represents earlier changes with presence of proinflammatory chemical mediators whereas MC Type II/III appear to represent more stable changes. Moreover, T2-mapping during aMR1 revealed differences in the loading effect for EPs associated with MCs that might reflect constrained EP-functionality. Also, the strong associations found between HIZ, MC and EP-changes may all reflect impairment in the motion segment. If the simultaneous presence of these MRI findings is linked to a more active ongoing inflammatory process and if this is related to a different pain pattern remains to be investigated.

Numerous studies have been performed with various results linking HIZ with spinal pain. This might be due to differences in the study protocols, e.g. differences in the ROI delineation and in the HIZ definition regarding the signal visibility in the T2-weighted as well as in the T1-weighted images for phenotyping of HIZ into double and single HIZ (20). The inconsistency found in the literature may also reflect a need for improved HIZ-phenotyping and that HIZ with a presence of associated EP and vertebral changes might represent an additional phenotype. Separation of EP-changes into subtypes, e.g calcifications, erosions and fissures, might also be relevant for the evaluation of spinal pain. In this study, EP-changes were only categorized into existing or non-existing findings using standardized MRI-methods with their intrinsic limitations in contrast and spatial resolution. Nevertheless, association were found. Non-cartesian MRI-methods have recently been developed for improved morphological visualization of the EPs (27). With the use of such methods, EP-phenotyping might be feasible.

Limitations

The small number of LBP-patients and thereby no possibility to relate these MRI findings to pain levels or pattern limits the strength of the conclusion. We, therefore, encourage
further larger studies to elucidate the clinical importance of the present findings.

In this study, the EP ROIs were positioned over the EP-zone, approximately one pixel from the visible edge of the IVD and vertebra to reduce the influence of these adjacent tissues on the EP T2-value. With use of such strategy, the segmentation does not rely on edges in the image for the delineation and this may affect the reproducibility of the T2-value. Nevertheless, the ICC displayed fair agreement between repeated measurements both within and between observers.

Conclusions

This study of LBP-patients suggests that HIZ is associated with simultaneous presence of both MCs and EP-changes in the same segment. Moreover, T2-mapping was found to objectively reflect MCs associated with HIZs and T2-mapping during aLMRI revealed functional behaviors of the EPs associated with MCs that might reflect impaired EP-functionality. If these three simultaneous morphological features are linked to an active inflammatory process, reflected as a clinical specific pain profile remains to be investigated.

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Tables

Table 1. Associations between the investigated morphological features given as absolute and relative numbers

| Feature   | HIZ=0 superior | HIZ=0 inferior | HIZ=1 superior | HIZ=1 inferior | MC=0 | MC=1 |
|-----------|----------------|----------------|----------------|----------------|------|------|
| MC        |                |                |                |                |      |      |
| =0        | 98 (86%)       | 106 (93%)      | 12 (57%)       | 15 (71%)       | -    | -    |
| =1        | 16 (14%)       | 8 (7%)         | 9 (43%)        | 6 (29%)        | -    | -    |
| EP change |                |                |                |                |      |      |
| =0        | 69 (61%)       | 84 (74%)       | 2 (10%)        | 6 (29%)        | 181 (70%) | 5 (13%) |
| =1        | 45 (40%)       | 30 (26%)       | 19 (91%)       | 15 (71%)       | 77 (30%) | 34 (87%) |

HIZ=High intensity zone, MC=Modic change of any type, EP=endplate. For the categorical variables, n is presented in absolute numbers and as percentage.

Figures
a) T1W- and b) T2W-images, displaying HIzs, MCs and EP-changes with a wide range of inhomogeneities of the signal in the EP-zone. Modic and discrete EP-changes, as well as HIz are seen at L4/L5. More extensive EP-changes are seen in EPs adjacent to the L5/S1 IVD.