GSplit LBI: Taming the Procedural Bias in Neuroimaging for Disease Prediction

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Abstract. In voxel-based neuroimage analysis, lesion features have been the main focus in disease prediction due to their interpretability with respect to the related diseases. However, we observe that there exist another type of features introduced during the preprocessing steps and we call them “Procedural Bias”. Besides, such bias can be leveraged to improve classification accuracy. Nevertheless, most existing models suffer from either under-fit without considering procedural bias or poor interpretability without differentiating such bias from lesion ones. In this paper, a novel dual-task algorithm namely GSplit LBI is proposed to resolve this problem. By introducing an augmented variable enforced to be structural sparsity with a variable splitting term, the estimators for prediction and selecting lesion features can be optimized separately and mutually monitored by each other following an iterative scheme. Empirical experiments have been evaluated on the Alzheimer’s Disease Neuroimaging Initiative (ADNI) database. The advantage of proposed model is verified by improved stability of selected lesion features and better classification results.

Keywords: · Voxel-based Structural Magnetic Resonance Imaging · Procedural Bias · Split Linearized Bregman Iteration · Feature selection

1 Introduction

Usually, the first step of voxel-based neuroimage analysis requires preprocessing the T₁-weighted image, such as segmentation and registration of grey matter (GM), white matter (WM) and cerebral spinal fluid (CSF). However, some systematic biases due to scanner difference and different population etc., can be introduced in this pipeline [2]. Part of them can be helpful to the discrimination of subjects from normal controls (NC), but may not be directly related to the disease. For example in structural Magnetic Resonance Imaging (sMRI) images of subjects with Alzheimer’s Disease (AD), after spatial normalization during simultaneous registration of GM, WM and CSF, the GM voxels surrounding lateral ventricle and subarachnoid space etc. may be mistakenly enlarged caused
by the enlargement of CSF space in those locations [2] compared to normal template, as shown in Fig. 1. Although these voxels/features are highly correlated with disease, they can’t be regarded as lesion features in an interpretable model. In this paper we refer to them as “Procedural Bias”, which should be identified but is neglected in the literature. We observe that it can be harnessed in our voxel-based image analysis to improve the prediction of disease.

![Fig. 1. The overlapped voxels among top 150 negative value voxels in each fold of $\beta_{pre}$ at the time corresponding to the best average prediction result in the path of GSplit LBI using 10-fold cross-validation. For subjects with AD, they represent enlarged GM voxels surrounding lateral ventricle, subarachnoid space, edge of gyrus, etc.](image)

Together with procedural bias, the lesion features are vital for prediction and lesion regions analysis tasks, which are commonly solved by two types of regularization models. Specifically, one kind of models such as general losses with $l_2$ penalty, elastic net [15] and graphnet [5] select strongly correlated features to minimize classification error. However, such models don’t differentiate features either introduced by disease or procedural bias and may also introduce redundant features. Hence, the interpretability of such models are poor and the models are prone to over-fit. The other kind of models with sparsity enforcement such as TV-$L_1$ (Combination of Total Variation [9] and $L_1$) and particularly $n^2$ GFL [13] enforce strong prior of disease on the parameters of the models introduced in order to capture the lesion features. Although such features are disease-relevant and the selection is stable, the models ignore the inevitable procedural bias, hence, they are losing some prediction power.

To incorporate both tasks of prediction and selection of lesion features, we propose an iterative dual-task algorithm namely Generalized Split LBI (GSplit LBI) which can have better model selection consistency than generalized lasso [11]. Specifically, by the introduction of variable splitting term inspired by Split LBI [6], two estimators are introduced and split apart. One estimator is for prediction and the other is for selecting lesion features, both of which can be pursued separately with a gap control. Following an iterative scheme, they will be mutually monitored by each other: the estimator for selecting lesion features is gradually monitored to pursue stable lesion features; on the other hand, the estimator for prediction is also monitored to exploit both the procedural bias and lesion features to improve prediction. To show the validity of the proposed method, we successfully apply our model to voxel-based sMRI analysis for AD, which is challenging and attracts increasing attention.
2 Method

2.1 GSplit LBI Algorithm

Our dataset consists of $N$ samples $\{x_i, y_i\}_1^N$ where $x_i \in \mathbb{R}^p$ collects the $i^{th}$ neuroimaging data with $p$ voxels and $y_i = \{\pm 1\}$ indicates the disease status ($-1$ for Alzheimer’s disease in this paper). $X \in \mathbb{R}^{N \times p}$ and $y \in \mathbb{R}^p$ are concatenations of $\{x_i\}_i$ and $\{y_i\}_i$. Consider a general linear model to predict the disease status (with the intercept parameter $\beta_0 \in \mathbb{R}$),

$$
\log P(y_i = 1|x_i) - \log P(y_i = -1|x_i) = x_i^T \beta_{\text{pre}} + \beta_0. \quad (2.1)
$$

A desired estimator $\beta_{\text{pre}} \in \mathbb{R}^p$ should not only fit the data by maximizing the log-likelihood in logistic regression, but also satisfy the following types of structural sparsity: (1) the number of voxels involved in the disease prediction is small, so $\beta_{\text{pre}}$ is sparse; (2) the voxel activities should be geometrically clustered or 3D-smooth, suggesting a TV-type sparsity on $\beta_{\text{pre}}$ component in $\beta$; (3) the degenerate GM voxels in AD are captured by nonnegative sparsity on $\beta_{\text{pre}}$. However, the existing procedural bias may violate these a priori sparsity properties, esp. the third one, yet increase the prediction power.

To overcome this issue, we adopt a variable splitting idea in [6] by introducing an auxiliary variable $\gamma \in \mathbb{R}^{[V[+1]]}$ to achieve these sparsity requirements separately, while controlling the gap from $D\beta_{\text{pre}}$ with penalty $S_\rho(\beta_{\text{pre}}, \gamma) := ||D\beta_{\text{pre}} - \gamma||_2^2 = ||\beta_{\text{pre}} - \gamma_n||_2^2 + ||\rho D_G \beta_{\text{pre}} - \gamma_G||_2^2$ with $\gamma = [\gamma_V \gamma_G]^T$ and $D = [I \rho D_G]^T$. Here $\rho$ controls the trade-off between different types of sparsity. Our purpose is thus of two-folds: (1) use $\beta_{\text{pre}}$ for prediction; (2) enforce sparsity on $\gamma$. Such a dual-task scheme can be illustrated by Fig. 6.

To implement it, we generalize the Split Linearized Bregman Iteration (Split LBI) algorithm in [6] to our setting with generalized linear models (GLM) and the three types of structural sparsity above, hence called Generalized Split LBI (or GSplit LBI). Algorithm 1 describes the procedure with a new loss:

$$
\ell(\beta_0, \beta_{\text{pre}}, \gamma; \{x_i, y_i\}_1^N, \nu) := \ell(\beta_0, \beta_{\text{pre}}; \{x_i, y_i\}_1^N) + \frac{1}{2\nu} S_\rho(\beta_{\text{pre}}, \gamma), \quad (2.2)
$$

where $\ell(\beta_0, \beta_{\text{pre}}; \{x_i, y_i\}_1^N)$ is the negative log-likelihood function for GLM and $\nu > 0$ tunes the strength of gap control. The algorithm returns a sequence of estimates as a regularization path, $[\beta_k, \gamma_{\text{pre}}, \gamma_k, \beta_{\text{les}}]_{k \geq 0}$. In particular, $\gamma_k$ shows a variety of sparsity levels and $\beta_{\text{pre}}$ is generically dense with different prediction powers. The projection of $\beta_{\text{pre}}$ onto the subspace with the same support of $\gamma_k$ gives estimate $\beta_{\text{les}}$, satisfying those a priori sparsity properties (sparse, 3D-smooth, nonnegative) and hence being regarded as the interpretable lesion features for AD. The remainder of this projection is heavily influenced by procedural bias; in

\[ D_G : \mathbb{R}^V \rightarrow \mathbb{R}^E \] denotes a graph difference operator on $G = (V, E)$, where $V$ is the node set of voxels, $E$ is the edge set of voxel pairs in neighbour (e.g. 3-by-3-by-3), such that $D_G(\beta)(i, j) := \beta(i) - \beta(j)$. 

\[ GSplit \text{ LBI: Taming the Procedural Bias in Neuroimaging} \]
Fig. 2. Illustration of \textit{GSplit LBI}. The gap between $\beta_{\text{pre}}$ for fitting data and $\gamma$ for sparsity is controlled by $S_{\rho}(\beta_{\text{pre}}, \gamma)$. The estimate $\beta_{\text{les}}$, as a projection of $\beta_{\text{pre}}$ on support set of $\gamma$, can be used for stable lesion features analysis when $\nu \to 0$ (Section 3.2). When $\nu \not\to 0$ (Section 3.1) with appropriately large value, $\beta_{\text{pre}}$ can be used for prediction by capturing both lesion features and procedural bias.

In this paper the non-zero elements in $\beta_{\text{pre}}^k$ which are negative (-1 denotes disease label) with comparably large magnitude are identified as procedural bias, while others with tiny values can be treated as nuisance or weak features. In summary, $\beta_{\text{les}}$ only selects lesion features; while $\beta_{\text{pre}}$ also captures additional procedural bias. Hence, such two kinds of features can be differentiated, as illustrated in Fig. 6.

2.2 Setting the Parameters

A stopping time at $t_k$ (line 10) is the regularization parameter, which can be determined via cross-validation to minimize the prediction error [7]. Parameter $\rho$ is a tradeoff between geometric clustering and voxel sparsity. Parameter $\kappa$, $\alpha$ is damping factor and step size, which should satisfy $\kappa \alpha \leq \nu / \kappa (1 + \nu \Lambda_H + \Lambda_H^2)$ to ensure the stability of iterations. Here $\Lambda_H$ denotes the largest singular value of a matrix and $H$ denotes the Hessian matrix of $\ell(\beta_0, \beta_{\text{pre}}; \{x_i, y_i\}_1^N)$.

Parameter $\nu$ balances the prediction task and sparsity enforcement in feature selection. In this paper, it is task-dependent, as shown in Fig. 6. For prediction of disease, $\beta_{\text{pre}}$ with appropriately larger value of $\nu$ may increase the prediction power by harnessing both lesion features and procedural bias. For lesion features analysis, $\beta_{\text{les}}$ with a small value of $\nu$ is helpful to enhance stability of feature selection. For details please refer to supplementary information.

3 Experimental Results

We apply our model to AD/NC classification (namely ADNC) and MCI (Mild Cognitive Impairment)/NC (namely MCINC) classification, which are two fundamental challenges in diagnosis of AD. The data are obtained from ADNI\textsuperscript{6}

\textsuperscript{6} http://adni.loni.ucla.edu
Algorithm 1 GSplit LBI

1: Input: Loss function $\ell(\beta_0, \beta_{\text{pre}}, \gamma; \{x_i, y_i\}_{i=1}^N, \nu)$, parameters $\nu, \rho, \kappa, \alpha > 0$.
2: Initialize: $k = 0$, $t^k = 0$, $\beta^k_0 = 0$, $\beta^k_{\text{pre}} = 0$, $\gamma^k_v = 0$, $\gamma^k_G = 0$, $z^k_0 = 0$, $z^k_\rho = 0$, $S_k := \supp(\gamma^k) = \emptyset$.
3: Iteration
4: $\beta^k_0 + 1 = \beta^k - \kappa \alpha \nabla \beta_0 \ell(\beta^k_0, \beta^k_{\text{pre}}, \gamma^k; \{x_i, y_i\}_{i=1}^N, \nu)$
5: $\beta^k_{\text{pre}} + 1 = \beta^k_{\text{pre}} - \kappa \alpha \nabla \beta_{\text{pre}} \ell(\beta^k_0, \beta^k_{\text{pre}}, \gamma^k; \{x_i, y_i\}_{i=1}^N, \nu)$
6: $z^{k+1} = z^k - (\kappa - \alpha \nabla \gamma \ell(\beta^k_0, \beta^k_{\text{pre}}, \gamma^k; \{x_i, y_i\}_{i=1}^N, \nu)$
7: $\gamma^{k+1}_V = \kappa \cdot S^+(z^{k+1}, 1)$, where $S^+(x, 1) = \max(x - 1, 0)$
8: $\gamma^{k+1}_G = \kappa \cdot S(\gamma^{k+1}_V, 1)$, where $S(x, 1) = \max(|x| - 1, 0)$
9: $\beta^k_{\text{les}} = P_{S_{k+1}} \beta^{k}_{\text{pre}}$, where $P_S = P_{\ker(D_S^c)} = I - D_S^c D_S^c$.
10: $t^{k+1} = (k + 1)\alpha$
11: Output: $\{\beta^k_0, \beta^k_{\text{pre}}, \beta^k_{\text{les}}, \gamma^k\}$, where $\beta^{k+1} = \left[\begin{array}{c} \gamma^{k+1}_V \\ \gamma^{k+1}_G \end{array}\right]$ and $z^{k+1} = \left[\begin{array}{c} z^{k+1}_0 \\ z^{k+1}_\rho \end{array}\right]$.

database, which is split into 1.5T and 3.0T (namely 15 and 30) MRI scan magnetic field strength datasets. The 15 dataset contains 64 AD, 208 MCI and 90 NC; while the 30 dataset contains 66 AD and 110 NC. DARTEL VBM pipeline [1] is then implemented to preprocess the data. Finally, the input features consist of 2,527 8x8x8 mm³ size voxels with average values in GM population template greater than 0.1. Experiments are designed on 15ADNC, 30ADNC and 15MCINC tasks.

3.1 Prediction and Path Analysis

10-fold cross-validation is adopted for classification evaluation. Under exactly the same experimental setup, comparison is made between GSplit LBI and other classifiers: SVM, MLDA (univariate model via t-test + LDA) [3], Graphnet [5], Lasso [10], Elastic Net, TV+L and $n^2$GFL. For each model, optimal parameters are determined by grid-search. For GSplit LBI, $\rho$ is chosen from $\{1, 2, ..., 10\}$, $\kappa$ is set to 10; $\alpha = \nu/\kappa(1 + \nu A^2_X + A^2_H)$; specifically, $\nu$ is set to 0.2 (corresponding to $\nu \rightarrow 0$ in Fig. 6). The regularization coefficient $\lambda$ is ranged in $\{0, 0.05, 0.1, ..., 0.95, 1, 10, 10^2\}$ for lasso⁹ and $2^{-10, -20, -30, ..., 0, ..., 20}$ for SVM. For other models, parameters are optimized from $\lambda : \{0.05, 0.1, ..., 0.95, 1, 10, 10^2\}$ and $\rho : \{0.5, 1, ..., 10\}$ (in addition, the mixture parameter $\alpha : \{0.05, 0.3, ..., 0.95\}$ for Elastic Net).

The best accuracy in the path of GSplit LBI and counterpart are reported. Table 1 shows that $\beta_{\text{pre}}$ of our model outperforms that of others in all cases. Note that although our accuracies may not be superior to models with multi-modality data [8], they are the state-of-the-art results for only sMRI modality.

⁷ For logit model, $\alpha < \nu/\kappa(1 + \nu A^2_X + \nu A^2_H)$ since $A^2_X > A^2_H$.

⁸ In this experiment, comparable prediction result will be given for $\nu \in (0.1, 10)$.

⁹ 0 corresponds to logistic regression model.
Table 1. Comparison of GSplit LBI with other models

|                | MLDA | SVM | Lasso | GraphNet | Elastic Net | TV + l1 | α²GFL | GSplit LBI (β_{pre}) |
|----------------|------|-----|-------|----------|-------------|--------|-------|---------------------|
| 15ADNC         | 86.06% | 83.12% | 87.01% | 86.36%  | 83.31% | 83.77% | 86.36% | 88.96%               |
| 30ADNC         | 86.93% | 87.50% | 87.50% | 88.64%  | 89.20% | 87.50% | 87.50% | 90.91%               |
| 15MCINC        | 61.41% | 70.13% | 69.80% | 72.15%  | 70.13% | 73.83% | 69.80% | 75.17%               |

Fig. 3. Left image: Accuracy of (β_{pre}, β_{les}) vs log t (t: regularization parameter). Right image: Six 2-d brain slice images of selected degenerative voxels of β_{les} and β_{pre} are sorted orderly at \{t_1, ..., t_6\}. As t grows, β_{pre} and β_{les} identify similar lesion features.

The process of feature selection combined with prediction accuracy can be analyzed together along the path. The result of 30ADNC is used as an illustration in Fig. 3. We can see that β_{pre} (blue curve) outperforms β_{les} (red curve) in the whole path for additional procedural bias captured by β_{pre}. Specifically, at β_{pre}’s highest accuracy (t_5), there is a more than 8% increase in prediction accuracy by β_{pre}. Early stopping regularization at t_5 is desired, as β_{pre} converges to β_{les} in prediction accuracy with overfitting when t grows. Recall that positive (negative) features represent degenerate (enlarged) voxels. In each fold of β_{pre} at t_5, the commonly selected voxels among top 150 negative (enlargement) voxels are identified as procedural bias shown in Fig. 1, where most of these GM voxels are enlarged and located near lateral ventricle or subarachnoid space etc., possibly due to enlargement of CSF space in those locations that are different from the lesion features.

3.2 Lesion Features Analysis

To quantitatively evaluate the stability of selected lesion features, multi-set Dice Coefficient (mDC)\footnote{In [13], mDC := \frac{10}{10} \sum_{k=1}^{10} \frac{|S(k)|}{|S(k)|} where S(k) denotes the support set of β_{les} in k-th fold.} \cite{4,13} is applied as a measurement. The 30ADNC task is again applied as an example, the mDC is computed for β_{les} which achieves highest accuracy by 10-fold cross-validation. As shown from Table 2, when \nu = 0.0002 (corresponding to \nu \rightarrow 0 in Fig. 6), the β_{les} of our model can obtain more stable lesion feature selection results than other models with comparable
prediction power. Besides, the average number of selected features (line 3 in Table 2) are also recorded. Note that although elastic net is of slightly higher accuracy than $\beta_{les}$, it selects much more features than necessary.

**Table 2.** mDC comparison between GSplit LBI and other models

| Model                | Accuracy | mDC   | $\sum_{k=1}^{10} |S(k)|/10 | $
|---------------------|----------|-------|--------------|
| Lasso               | 87.50%   | 0.1992| 50.2         |
| Elastic Net         | 89.20%   | 0.5631| 777.8        |
| Graphnet            | 88.64%   | 0.6005| 832.6        |
| TV + $l_1$          | 87.50%   | 0.5824| 712.6        |
| n² GFL              | 87.50%   | 0.5362| 443.9        |
| GSplit LBI ($\beta_{les}$) | 88.64%   | 0.7805| 129.4        |

For the meaningfulness of selected lesion features, they are shown in Fig. 4 (a)-(c), located in hippocampus, parahippocampal gyrus and medial temporal lobe etc., which are believed to be early damaged regions for AD patients.

![Fig. 4](image)

(a) fold 2  (b) fold 10  (c) overlap  (d) coarse-to-fine

Fig. 4. (a)-(c): Stability of selected lesion features of $\beta_{les}$ shown in 2-d 110 slice brain images when $\nu = 0.0002$. (a)-(b): Results of fold 2 and fold 10. (c): The overlapped features in 10 folds. (d): The 2-d slice brain image of selected voxels with $2 \times 2 \times 2$ mm$^3$ using coarse-to-fine approach.

To further investigate the locus of lesion features, we conduct a coarse-to-fine experiment. Specifically, we project the selected overlapped voxels of $8 \times 8 \times 8$ mm$^3$ size (shown in Fig. 4 (c)) onto MRI image with more finer scale voxels, i.e. in size of $2 \times 2 \times 2$ mm$^3$. Totally 4,895 voxels are served as input features after projection. Again, the GSplit LBI is implemented using 10-fold cross-validation. The prediction accuracy of $\beta_{pre}$ is 90.34% and on average 446.6 voxels are selected by $\beta_{les}$. As desired, these voxels belong to parts of lesion regions, such as those located in hippocampal tail, as shown in Fig. 4 (d).

4 Conclusions

In this paper, a novel iterative dual task algorithm is proposed to incorporate both disease prediction and lesion feature selection in neuroimaging analysis.
With variable splitting term, the estimators for prediction and selecting lesion features can be separately pursued and mutually monitored under a gap control. The gap here is dominated by procedural bias, some specific features crucial for prediction yet ignored in a priori disease knowledge. With experimental studies conducted on 15ADNC, 30ADNC and 15MCINC tasks, we have shown that the leverage of procedural bias can lead to significant improvements in both prediction and model interpretability. In future works, we shall extend our model to other neuroimaging applications including multi-modality data.

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Supplementary Information

A Notation

For matrix $A$, $A_{ij}$ represents the submatrix of $A$ indexed by $J$. $A^\dagger$ denotes the Moore-Penrose pseudoinverse of $A$. Suppose $A \in \mathbb{R}^{m \times p}$, $\|A\|_\Sigma := \text{trace}(A) = \sum_{i=1}^m A_{i,i}$. Besides, $\beta$ and $\beta$ are used to represent $\beta_{ics}$ and $\beta_{pre}$ respectively in what follows.

B Model selection consistency

Consider recovery from generalized linear model(GLM) of $\beta^\star \in \mathbb{R}^p$ which satisfies structural sparsity after linearly transformed by $D \in \mathbb{R}^{m \times p}$:

$$P(y|x, \beta^\star) \propto \exp\left(\frac{x^T \beta^\star - \psi(x^T \beta^\star)}{d(\sigma)}\right)$$

$$\text{subject to } \gamma = D \beta^\star \quad (S := \text{supp}(\gamma^\star), s = |S|, s < m) \quad (B.1)$$

where $\psi: \mathbb{R} \to \mathbb{R}$ is link function and $d(\sigma)$ is known parameter related to the variance of distribution.

Under linear model with $\psi(t) = t^2$ and $d(\sigma) = \sigma^2$ in B.1, our model GSplit LBI degenerates to Split LBI [6]. Recently, it’s proved in [6] that the Split LBI may achieve model selection consistency under weaker conditions than generalized lasso [11,12] if $\nu$ is large enough. We claim that this property can also be shared by logit model.

To understand why Gsplit LBI can achieve better model selection consistency, note that the variable splitting term projects solution vector $\beta$ into higher dimensional space $(\beta, \gamma)$ with $\beta$ fitting data and $\gamma$ being structural sparse. This will make it easier for the subspace of $\gamma_{S^c}$ to decorrelate with the subspace of $(\beta, \gamma_S)$, especially when $\nu$ increases, which sheds light on better performance of Split LBI to recover true signal set $S$. What’s more important, the property may also be shared by logit model when $y = \{\pm 1\}, d(\sigma) = 1$ and $\psi(t) = \log(1 + exp(t))$. Concretely speaking, we use $\theta_{S^c,(\beta,\gamma)}(\nu)$ to denote the angle between subspace of $\gamma_{S^c}$ and that of $(\beta, \gamma_S)$, the definition of which is:

$$\theta_{S^c,(\beta,\gamma)}(\nu) := \arccos\left(\frac{\|P_{A_{\beta,\gamma}} A_{S^c}\|_F}{\|A_{S^c}\|_F}\right) = \arccos\left(\sqrt{\frac{\|H_{S^c,(\beta,\gamma)} H_{(\beta,\gamma),S^c}\|_\Sigma^\dagger}{\|H_{S^c,S^c}\|_\Sigma}}\right) \quad (B.2)$$

Where $A := [A_{(\beta,\gamma)} A_{S^c}]$ and $H := \nabla^2_{\beta,\gamma} l(\beta, \gamma) = A^T A = \begin{bmatrix} H_{(\beta,\gamma),(\beta,\gamma)} & H_{(\beta,\gamma),S^c} \\ H_{S^c,(\beta,\gamma)} & H_{S^c,S^c} \end{bmatrix}$.

Remark 1. For linear model, $A = \nabla_{\beta,\gamma} l(\beta, \gamma)$ with

$$A_{(\beta,\gamma)} = \begin{bmatrix} X_{n \times p}^{1/2} & 0_{n \times s} \\ -D_{S^c}/\sqrt{\nu} I_{(S^c),S^c}/\sqrt{\nu} & 0_{(p-s) \times s} \end{bmatrix} \quad A_{S^c} = \begin{bmatrix} 0_{n \times (p-s)} \\ 0_{s \times (p-s)} \end{bmatrix} \quad (B.3)$$
There is no explicit definition for $A$ for logit model, however $\theta_{S^c,(\beta,S)}(\nu)$ can be computed through Hessian matrix $H$ in equation B.3.

We claim that $\theta_{S^c,(\beta,S)}(\nu)$ will increase as $\nu$ becomes larger under some conditions. See theorem 1 for details.

**Theorem 1.** Under linear model and logit model, $\lim_{\nu \to +\infty} \theta_{S^c,(\beta,S)}(\nu) = 90^\circ$ if and only if $\text{Im}(D_{S^c}^T) \subseteq \text{Im}(X^T)$.

**Remark 2.** In [6], it’s been proved that the necessary condition for sign-consistency is $\text{IRR}(\nu) < 1$. For uniqueness of model, we also assume that $\ker(X) \cap \ker(D_{S^c}) \subseteq \ker(D_S)$. Combined with $\text{Im}(D_{S^c}^T) \subseteq \text{Im}(X^T)$ $\iff$ $\ker(X) \subseteq \ker(D_{S^c})$, we have that $\ker(X) \subseteq \ker(D_S)$, which is the sufficient and necessary condition for the hold of $\lim_{\nu \to +\infty} \text{IRR}(\nu) \to 0$. Hence, this is another way to understand why GSplit LBI can achieve better model selection consistency.

**Proof.** We firstly prove the case under linear model. Denoted $A := \nu X^* + D^T D$ where $X \in \mathbb{R}^{m \times p}$ and $X^* = X/n$. Note that:

$$H_{(\beta,S)} = QLQ^T, \quad H_{S^c,(\beta,S)} = [D_{S^c}/\nu 0]$$

where:

$$Q = \begin{bmatrix} I_p & 0 \\ -D_S A^\dagger I_s \end{bmatrix}, \quad L = \begin{bmatrix} A/\nu & 0 \\ 0 & (I_s - D_S A^\dagger D_S^T)/\nu \end{bmatrix}$$

(B.4)

Then we have:

$$H_{S^c,(\beta,S)} H_{(\beta,S),(\beta,S)} H_{(\beta,S),S^c} = H_{S^c,(\beta,S)} QLQ^T H_{(\beta,S),S^c} = \frac{1}{\nu} D_{S^c} A^\dagger D_{S^c}^T$$

(B.5)

Substituting equation B.5 into the second equation of B.2, we have:

$$\cos^2(\theta_{S^c,(\beta,S)}(\nu)) = \frac{\|D_{S^c} A^\dagger D_{S^c}\|_\Sigma}{\|H_{S^c,(\beta,S)}\|_\Sigma} = \frac{\|D_{S^c} A^\dagger D_{S^c}\|_\Sigma}{m - s}$$

(B.6)

Denote $e_i \in \mathbb{R}^{m-s}$ as the vector with the $i^{th}$ element being 1 and left being 0. Then equation B.6 is equivalent to:

$$\cos^2(\theta_{S^c,(\beta,S)}(\nu)) (m - s) = \sum_{i=1}^p d_i^T A^\dagger d_i$$

(B.7)

where $d_i := D_{S^c}^T e_i$. Suppose the compact singular value decomposition of $X/\sqrt{n} := UAV^T$, and $(V, \tilde{V})$ be an orthogonal square matrix. Suppose the compact singular value decomposition of $D\tilde{V} := U_1 A_1 V_1^T$. If $\text{Im}(D_{S^c}^T) \subseteq \text{Im}(X^T)$, then $\exists f_i$, such that $d_i = V f_i$, hence,

$$d_i^T (\nu X^* X + D^T D)^\dagger d_i = d_i^T (V \tilde{V}) \left( (V^T (\nu X^* X + D^T D) (V \tilde{V}) \right)^\dagger (V^T) d_i$$

$$= f_i^T (\nu A^2 + V^T D^T D V)^{-1} f_i \to 0, \text{ as } \nu \to \infty$$

(B.8)
Combined with equation B.7, it’s then easy to obtain that \( \cos^2(\theta_{S^*}(\beta,S)(\nu)) \to 0 \) as \( \nu \to +\infty \). On the contrary, if \( \exists \alpha \) such that \( D_{S}^T\alpha \notin \text{Im}(X^T) \), then there \( \exists i^* \) such that \( d_{i^*} \notin \text{Im}(X^T) \). This means that for \( d_{i^*} \), there \( \exists f_1,i^*, f_2,i^* \neq 0 \) such that \( d_{i^*} = Vf_1,i^* + \tilde{V}f_2,i^* \). Then we have

\[
d_{i^*}^T(\nu X^*X + D^TD)d_{i^*} \geq f_2,i^*,(\tilde{V}^TD^TD\tilde{V})f_2,i^* = f_2,i^*,V_1A_1^{-2}V_1^TF_{2,i^*}.
\]

do not equal to 0 \( \iff f_2,i^*,V_1A_1^{-2}V_1^TF_{2,i^*} = f_2,i^*,\tilde{V}^TD^TD\tilde{V}f_{2,i^*} \neq 0 \). Since

\[
f_{2,i^*}\tilde{V}^TD^TD\tilde{V}f_{2,i^*} \geq f_2,i^*,\tilde{V}^Td_{i^*},d_{i^*},f_{2,i^*} = (f_{2,i^*}f_{2,i^*})^2 > 0
\]

From equation B.7, we can obtain that:

\[
\cos^2(\theta_{S^*}(\beta,S)(\nu))(m - s) \geq d_{i^*}^TA^*d_{i^*} \neq 0
\]

which means that \( \theta_{S^*}(\beta,S)(\nu) \to 0 \) does not hold when \( \nu \to +\infty \). The proof is then completed under linear model. Under logit model, the definition of \( A \) is modified to \( A := \nu X^*W((x_i,\beta)^p_{i=1})X + D^TD \) where \( W((x_i,\beta)^p_{i=1}) \) is a diagonal matrix with each diagonal element equals to \( \frac{\exp(x_i^T\beta)}{1+\exp(x_i^T\beta)} \), the left proof is almost the same with that of linear model.

An simulation experiment is conducted to illustrate this idea. In more detail, \( n = 100 \) and \( p = 80 \), \( D = I \) and \( X \in \mathbb{R}^{n \times p} \) and \( X_{i,j} \sim N(0,1) \). \( \beta^*_i = 2 \) for \( 1 \leq i \leq 4 \), \( \beta^*_i = -2 \) for \( 5 \leq i \leq 8 \) and 0 otherwise, \( y \) is generated by both linear model \( y = X\beta^* + \epsilon \) with \( \epsilon \sim N(0,1) \) and logit model given \( X \) and \( \beta^* \). We simulated for 100 times and average \( \theta_{S^*}(\beta,S)(\nu) \) is then computed, which is shown in the left image in figure 5. We can see that \( \theta_{S^*}(\beta,S)(\nu) \) increases when \( \nu \) becomes larger, as illustrated in right image in figure 5, and converges to 90° when \( \nu \to +\infty \). The average AUC and estimation of \( \beta^* \) of Gsplit LBI with different \( \nu \) compared with those of genlasso are also computed. Table B shows better AUC with the increase of \( \nu \) before \( \nu = 100 \). As we can see from the algorithm in the paper that \( \hat{\beta} \) is the projection of \( \beta \) onto the support set of \( \gamma \). Hence it is equivalent to say that better model selection of \( \hat{\beta} \) can be achieved as \( \nu \) increases.

However, the excessively large value of \( \nu \) will lower the signal-to-noise ratio, which is also crucial for model selection consistency and prediction estimation. It’s shown in [6] that \( \nu \) determines the trade-off between model selection consistency and estimation of \( \beta^* \). Also, the irrepresentable condition(IRR) can be satisfied as long as \( \nu \) is large enough. If \( \nu \) continuously increase, it will deteriorate the estimation of \( \beta^* \), prediction estimation and even AUC. In our experiment the same phenomena can be observed, i.e. the estimation of \( \hat{\beta} \) and \( \beta \) get worse if \( \nu \) increases from 10 and 100, respectively; when \( \nu = 100 \), AUC even decreases.

### C Relationship between \( \beta \) and \( \hat{\beta} \)

The estimate \( \hat{\beta} \), as a projection of \( \beta \) onto the subspace of \( \gamma \), can select features that satisfy structural sparsity. Following the Linearized Bregman Iteration [14],
Angle between subspace of $\gamma_S$ and $(\beta, \gamma_S c)$

\[ \theta_{S^c(\beta,S)}(\nu) \]

Fig. 5. Left image: The $\theta_{S^c(\beta,S)}(\nu)$ curve of logit model and linear model. Right image: Illustration of $\theta_{S^c(\beta,S)}(\nu)$ and it monotonically increase v.s. $\nu$.

Table 3. Comparison between Gsplit LBI with different $\nu$ and genlasso in terms of AUC, $\|\hat{\beta} - \beta^*\|_2$, $\|\beta - \beta^*\|_2$, $\|X\hat{\beta} - X\beta^*\|_2$ and $\|X\beta - X\beta^*\|_2$.

| \( \nu \) | Gsplit LBI | genlasso |
| --- | --- | --- |
| 0.02 | 0.9531 | 0.98194 |
| 0.1 | 0.9854 | 0.98791 |
| 1 | 0.98792 | 0.98590 |
| 5 | 0.98590 | 0.97915 |
| 10 | 0.98792 | 0.98590 |
| 100 | - | - |

$\beta$ and $\hat{\beta}$ will be more similar on features selected by $\hat{\beta}$. In more detail, note that when $t = 0$, $\hat{\beta}(t) = 0$ and $\beta(t)$ is the graph laplacian regularizer with penalty factor $\frac{1}{\nu}$. As $t$ progresses, the gap between $\beta(t)$ and $\hat{\beta}(t)$ will decrease in terms of $\|\beta(t) - \hat{\beta}(t)\|_2$ for every $\nu$, as shown in figure 6.

Fig. 6. $\|\beta - \hat{\beta}\|_2$ in the regularized solution path when $\nu = 100, 1, 0.02$. As $\nu$ decreases, the distance of $\beta(t)$ and $\hat{\beta}(t)$ are tended to be with smaller distance.
Fig. 7. Comparison of regularized solution path between $\beta$ and $\tilde{\beta}$ when $\nu = 100, 1, 0.02$. They look more similar with each other as $\nu$ decreases.

Since $\| \beta(t) - \tilde{\beta}(t) \|_2 \to 0$ as $t \to +\infty$ and $\tilde{\beta}$ is sparse, it follows that $\beta$ will approximate to $\tilde{\beta}$ on those selected features. In addition to these selected features, before convergence to $\tilde{\beta}$, $\beta$ can capture other features to better fit data (minimize training error), especially for those ones that significantly correlated with data.

D Choice of $\nu$

The choice of $\nu$ is task-dependent. For stable feature selection, $\nu$ with rather "small" value is suggested. It’s noted that $\beta - \tilde{\beta} \to 0$ as $\nu \to 0^+$, which is reflected by $l_2$ norm and regularized solution path shown in figure 6, 7. In this case, the estimator $\tilde{\beta}$ will be constrained in comparably lower dimension space, therefore it may fit data with more stability, notwithstanding $\beta$ have no ability to select other features.

For prediction estimation, the appropriately large value of $\nu$ is preferred. On one hand, when $\nu$ is appropriately large, the ability of selecting features with better model selection consistency can be achieved and $\beta$ will share closer values on these selected features as $t$ progress, as shown in figure 7. On the other hand, $\beta$ may increase the ability of fitting data by having other features being non-zeros as long as $\nu$ is not too small. In fact, it is shown in table B that comparable results can be given as long as $\nu$ belongs to a reasonable range of values (0.1-10 in this case).

E IDS of ADNI subject used in our experiments

| Subject | ID   | Class | Subject | ID   | Class | Subject | ID   | Class |
|---------|------|-------|---------|------|-------|---------|------|-------|
| 123_S_0094 | 9655 | 15AD | 927_S_0408 | 14964 | 15MCI | 072_S_0315 | 12559 | 15NC |
| Patient ID | Age | Sex | Diagnosis | FDG-PET Score | Gray Matter Score | White Matter Score | Duration |
|------------|-----|-----|-----------|---------------|------------------|-------------------|----------|
| S_0179     | 027 |     | MCI       | 127 S_1427    | 69355 S_15MCI    | 100 S_4511       | 289653   |
| S_0231     | 021 |     | MCI       | 037 S_1421    | 70885 S_15MCI    | 012 S_4545       | 290413   |
| S_0249     | 007 |     | MCI       | 137 S_1426    | 72082 S_15MCI    | 053 S_4578       | 290814   |
| S_0269     | 098 |     | MCI       | 116 S_0041    | 8177 S_15MCI     | 127 S_4604       | 291523   |
| S_0289     | 130 |     | MCI       | 118 S_0050    | 8648 S_15MCI     | 007 S_4620       | 293938   |
| S_0273     | 021 |     | MCI       | 119 S_0006    | 8793 S_15MCI     | 127 S_4645       | 295590   |
| S_0293     | 007 |     | MCI       | 119 S_0101    | 9093 S_15MCI     | 014 S_4579       | 296776   |
| S_0294     | 007 |     | MCI       | 120 S_0035    | 9120 S_15MCI     | 014 S_4580       | 296859   |
| S_0276     | 128 |     | MCI       | 121 S_0047    | 9899 S_15MCI     | 012 S_4642       | 296878   |
| S_0275     | 027 |     | MCI       | 122 S_0067    | 9903 S_15MCI     | 012 S_4643       | 297693   |
| S_0285     | 130 |     | MCI       | 124 S_0043    | 9324 S_15MCI     | 029 S_4585       | 298523   |
| S_0288     | 098 |     | MCI       | 126 S_0069    | 9417 S_15MCI     | 013 S_4616       | 300089   |
| S_0344     | 007 |     | MCI       | 126 S_0095    | 9680 S_15MCI     | 029 S_4652       | 300886   |
| S_0332     | 021 |     | MCI       | 128 S_0072    | 9752 S_15MCI     | 137 S_4632       | 301677   |
| S_0258     | 128 |     | MCI       | 130 S_0070    | 10027 S_15MCI    | 094 S_4649       | 302926   |
| S_0307     | 027 |     | MCI       | 131 S_0123    | 10043 S_15MCI    | 016 S_4638       | 305882   |
| S_0390     | 123 |     | MCI       | 133 S_0118    | 11370 S_15MCI    | 013 S_4731       | 308178   |
| S_0351     | 031 |     | MCI       | 137 S_0172    | 11398 S_15MCI    | 136 S_4726       | 308396   |
| S_0423     | 021 |     | MCI       | 139 S_0232    | 11567 S_15MCI    | 016 S_4688       | 310327   |
| S_0389     | 053 |     | MCI       | 139 S_0223    | 11645 S_15MCI    | 019 S_4835       | 315857   |
| S_0434     | 094 |     | MCI       | 139 S_0113    | 11714 S_15MCI    | 127 S_4843       | 316771   |
| S_0401     | 068 |     | MCI       | 141 S_0230    | 11806 S_15MCI    | 003 S_4839       | 319414   |
| S_0409     | 131 |     | MCI       | 142 S_0283    | 12028 S_15MCI    | 003 S_4840       | 319427   |
| S_0361     | 116 |     | MCI       | 142 S_0245    | 12242 S_15MCI    | 003 S_4872       | 321376   |
| S_0339     | 132 |     | MCI       | 143 S_0272    | 12313 S_15MCI    | 003 S_4900       | 325729   |
| S_0377     | 037 |     | MCI       | 144 S_0229    | 12459 S_15MCI    | 016 S_4951       | 337692   |
| S_0485     | 027 |     | MCI       | 149 S_0337    | 12466 S_15MCI    | 016 S_4951       | 337692   |
| S_0102     | 130 |     | MCI       | 098 S_0171    | 10818 S_15MCI    | 016 S_4951       | 337692   |