Detection of Pancreatic Carcinomas by Imaging Lactose-Binding Protein Expression in Peritumoral Pancreas Using \([^{18}F]\)Fluoroethyl-Deoxylactose PET/CT

Leo Garcia Flores¹, Susanna Bertolini¹, Hsin Hsin Yeh¹, Daniel Young¹, Uday Mukhopadhyay¹, Ashutosh Pal¹, Yunming Ying³, Andrei Volgin¹, Aleksandr Shavrin¹, Suren Soghomonyan¹, William Tong¹, William Bornmann³, Mian M. Alauddin¹, Craig Logsdon², Juri G. Gelovani¹*

¹ Department of Experimental Diagnostic Imaging, Center for Advanced Biomedical Imaging Research (CABIR), The University of Texas MD Anderson Cancer Center, Houston, Texas, United States of America, ² Department of Cancer Biology, The University of Texas MD Anderson Cancer Center, Houston, Texas, United States of America, ³ Department of Experimental Therapeutics, The University of Texas MD Anderson Cancer Center, Houston, Texas, United States of America

Abstract

**Background:** Early diagnosis of pancreatic carcinoma with highly sensitive diagnostic imaging methods could save lives of many thousands of patients, because early detection increases resectability and survival rates. Current non-invasive diagnostic imaging techniques have inadequate resolution and sensitivity for detection of small size (~2–3 mm) early pancreatic carcinoma lesions. Therefore, we have assessed the efficacy of positron emission tomography and computer tomography (PET/CT) imaging with \(\beta\)-D-galactopyranosyl-(1,4\(^{-}\))-2-deoxy-2-\([^{18}F]\)fluoroethyl-D-glucopyranose (\([^{18}F]\)FEDL) for detection of less than 3 mm orthotopic xenografts of L3.6pl pancreatic carcinomas in mice. \([^{18}F]\)FEDL is a novel radioligand of hepatocarcinoma-intestine-pancreas/pancreatitis-associated protein (HIP/PAP), which is overexpressed in peritumoral pancreatic acinar cells.

**Methodology/Principal Findings:** Dynamic PET/CT imaging demonstrated rapid accumulation of \([^{18}F]\)FEDL in peritumoral pancreatic tissue (4.04 ± 2.06%ID/g), bi-exponential blood clearance with half-lives of 1.65 ± 0.50 min and 14.14 ± 3.60 min, and rapid elimination from other organs and tissues, predominantly by renal clearance. Using model-independent graphical analysis of dynamic PET data, the average distribution volume ratio (DVR) for \([^{18}F]\)FEDL in peritumoral pancreatic tissue was estimated as 3.57 ± 0.60 and 0.94 ± 0.72 in sham-operated control pancreas. Comparative analysis of quantitative autoradiographic images and densitometry of immunohistochemically stained and co-registered adjacent tissue sections demonstrated a strong linear correlation between the magnitude of \([^{18}F]\)FEDL binding and HIP/PAP expression in corresponding regions (r = 0.88). The in situ analysis demonstrated that at least a 2–4 fold apparent lesion size amplification was achieved for submillimeter tumors and to nearly half a murine pancreas for tumors larger than 3 mm.

**Conclusion/Significance:** We have demonstrated the feasibility of detection of early pancreatic tumors by non-invasive imaging with \([^{18}F]\)FEDL PET/CT of tumor biomarker HIP/PAP over-expressed in peritumoral pancreatic tissue. Non-invasive non-invasive detection of early pancreatic carcinomas with \([^{18}F]\)FEDL PET/CT imaging should aid the guidance of biopsies and additional imaging procedures, facilitate the resectability and improve the overall prognosis.

Introduction

The estimated number of new cases of pancreatic cancer in the United States in 2009 is 42,470 and the estimated number of deaths is 35,240 [1]. Although, pancreatic cancer accounts for only 2% of all malignancies, it is the fourth most common cause of cancer death in the United States. Such a poor prognosis for patients with pancreatic cancer is because 80–90% of patients have unresectable disease at the time of diagnosis [2]. It is widely accepted that the overall and disease-free survival of patients with pancreatic carcinoma are related to the possibility of complete macroscopic R0 resection [3]. Prognosis is also related to tumor size (<30 mm), nodal involvement and resection margin status [4]. Therefore, early diagnosis of pancreatic carcinoma with highly sensitive diagnostic imaging methods is very important and could save lives of many thousands of patients, because early detection of small pancreatic cancers is likely to increase resectability rates.

Due to inadequate resolution and sensitivity of \([^{18}F]\)-FDG PET/CT imaging (~5 mm in plane) for detection of small size (~2–3 mm) early pancreatic carcinoma lesions [5], we have focused on the development of imaging agents for visualization of tumor-induced biomarkers that are over-expressed in the peritumoral...
pancreatic tissue. Such an approach should generate the “lesion size amplification” effect and result in at least 3 to 4 fold increase in the apparent lesion size. Such an approach could potentially improve the overall detectability of pancreatic tumor lesions at early stages of their development, improve their respectability, and the overall prognosis.

Among pancreatic tumor biomarkers produced in peritumoral reactive pancreatic tissue, the hepatocarcinoma-intestine-pancreas/pancreatitis-associated protein (HIP/PAP) was found to be over-expressed more than 130-fold in pancreatic acinar cells, as compared to normal pancreas [6]. In contrast, only a 9-fold increased expression of HIP/PAP protein was observed in acinar cells in chronic pancreatitis. Also, fragments of HIP/PAP protein are immunodetectable in blood and their levels correlate with the severity of pancreatic inflammation and pancreatic carcinoma size [7]. Furthermore, HIP/PAP protein is a promising target for the development of imaging agents, because it is also overexpressed in hepatocellular and cholangial carcinomas within the tumor cells [8].

The HIP/PAP protein is a 16 kD secreted protein, which belongs to the group VII of a family of proteins that contain a C-type lectin domain, according to Drickamer’s classification [9], which binds carbohydrates, and that it is also known as the “lactose-binding protein” (for review [10]. Previous biochemical studies demonstrated that GST-purified recombinant HIP/PAP protein has a very high affinity to D-lactose, but insignificantly to D-glucopyranose, D,L-fucose, D-galactopyranose, or N-acetyl-β-D-glucosamine [11]. We hypothesized, that the HIP/PAP (the lactose-binding protein) should bind minimally modified 18F-labeled lactose analogues with high affinity, and that this “receptor-ligand” binding type of an imaging approach should allow for visualization of peritumoral infiltrated pancreatic tissue that 130-fold over-expresses the HIP/PAP protein, as compared to normal pancreatic tissue.

Dynamic PET imaging demonstrated a rapid accumulation of [18F]FEDL in the area of L3.6pl/GL+ tumor growth with characteristically concentric or a horseshoe pattern (Fig. 2A–C), which corresponds to the pancreatic tail adjacent to the visceral surface of the spleen and anterior to the upper pole of the left kidney. Model-independent graphical analysis of dynamic PET imaging data (Logan plot) using muscle as the reference tissue allowed for visualization of peritumoral infiltrated pancreatic tissue that 130-fold over-expresses the HIP/PAP protein, as compared to normal pancreatic tissue.

In vivo 18F-FEDL Autoradiography and HIP/PAP Expression

In situ validation of in vivo 18F-FEDL PET/CT imaging was performed at the end of each dynamic imaging study using comparative analysis with autoradiography and immunohistochemical analysis. We conclude, that non-invasive detection of early pancreatic carcinomas with 18F-FEDL PET/CT imaging should aid the guidance of biopsies and additional imaging procedures, facilitate the resectability and improve the overall prognosis.

**Results**

**Orthotopic Pancreatic Tumor Xenograft Model**

In the Group I mice (N = 12), non-invasive bioluminescence imaging (BLI) was used for monitoring the growth of orthotopic pancreatic carcinoma xenografts. Distinct bioluminescence imaging (BLI) signal was detectable in the area consistent with the site of the L3.6pl/GL+ cell injection already on day 4 (Fig. 1A) and increased exponentially by day 10 post injection (Fig. 1A,B). Based on the results of BLI, PET/CT imaging studies in Group I, subsequent PET/CT imaging studies with 18F-FEDL were performed 7 days after injection of L3.6pl/GL+ cells, when the tumor diameter was 1.8±0.9 mm. However, based on the IHC analysis of pancreatic tissue sections, the apparent diameter of the lesion based on the expression of HIP/PAP in peritumoral pancreatic tissue ranged from 2 mm for sub-millimeter sized tumors (Fig. 1C) to almost a half of the pancreas (10–12 mm) for tumors of 2–3 mm in diameter. In all cases, at least a 2–4 fold amplification of the apparent tumor lesion size was observed, based on the extent of HIP/PAP expression in the peritumoral pancreas.

**PET/CT with 18F-FEDL**

Dynamic PET imaging demonstrated a rapid accumulation of [18F]FEDL in the area of L3.6pl/GL+ tumor growth with characteristically concentric or a horseshoe pattern (Fig. 2A–C), which corresponds to the pancreatic tail adjacent to the visceral surface of the spleen and anterior to the upper pole of the left kidney. Model-independent graphical analysis of dynamic PET imaging data (Logan plot) using muscle as the reference tissue allowed for visualization of peritumoral infiltrated pancreatic tissue that 130-fold over-expresses the HIP/PAP protein, as compared to normal pancreatic tissue.
was conducted using frozen pancreatic tissue sections obtained from mice bearing small orthotopic xenografts of L3.6pl/GL+ tumors (Fig. 4A). The autoradiographic images demonstrated a peritumoral pattern of $^{[18F]}$FEDL binding to the reactive pancreatic tissue (blue rectangle Fig. 4B, shown magnified in 4E), which was consistent with the high level of HIP/PAP expression observed in peritumoral pancreatic tissue in the corresponding area (Fig. 4H). In contrast, the magnitude of $^{[18F]}$FEDL binding pancreatic tissue was significantly lower in the regions remote from the site of tumor growth (red rectangle Fig. 4B, shown magnified in 4D), which was consistent with low (background levels of HIP/PAP expression in these remote regions of pancreas (Fig. 4G). Pre-treatment of an adjacent tissue section with 1 mM lactose resulted in a complete inhibition of specific binding of $^{[18F]}$FEDL to pancreatic tissue (Fig. 4C). However, some non-specific binding was still observed, which had punctuate or small circular pattern the origins of which is, presumably, the intimal layer of larger vessels and intestinal content (blue rectangle Fig. 4C, magnified in 4F). Comparative densitometric analysis of autoradiographic and IHC images demonstrated a good linear correlation ($r = 0.88$) between the magnitude of $^{[18F]}$FEDL binding and the level of HIP/PAP protein expression in different regions (Fig. 4I).

**Discussion**

In the current study, we have demonstrated that the detection of early stage pancreatic carcinomas is feasible using PET/CT with $^{[18F]}$FEDL, a radioligand for HIP/PAP, which is selectively over-expressed in peritumoral pancreatic acinar cells. The extent of HIP/PAP over-expression in peritumoral pancreas resulted in a significant amplification of the apparent lesion size: at least a 2–4 fold amplification of the apparent tumor lesion size for sub-millimeter sized tumors to almost a half of the pancreas (10–12 mm) for tumors of 2–2.5 mm in diameter. The magnitude of peritumoral accumulation of $^{[18F]}$FEDL was proportional to the level of HIP/PAP expression ($r = 0.88$), as demonstrated by a comparative densitometric analysis of QAR and IHC-stained tissues sections. It is noteworthy, that such relationship with HIP/PAP expression was observed using QAR after *in vivo* intravenous administration of $^{[18F]}$FEDL (after PET/CT imaging) as well as using *ex vivo* QAR (after incubation of frozen tissue section in solution with $^{[18F]}$FEDL). The specificity of $^{[18F]}$FEDL binding was confirmed by pre-blocking of the tissue sections with excess of non-radiolabeled lactose. Together, these results further confirm the specificity of $^{[18F]}$FEDL binding to the HIP/PAP protein-expressing peritumoral pancreatic tissue.

To quantify the magnitude of $^{[18F]}$FEDL binding to peritumoral pancreatic tissue, we elected to utilize model-independent Logan graphical analysis, due to the limitations of repetitive blood sampling in mice, which hampers the radiolabeled metabolite analysis from small volumes of plasma. Instead of the arterial blood input function, the Logan graphical analysis utilizes time-activity data from a reference tissue [14]. Ideally, normal
pancreatic tissue not expressing the HIP/PAP should be used as the reference tissue for peritumoral pancreatic tissue. However, the results of our studies using in situ QAR and IHC demonstrated in some cases a fairly extensive over-expression of HIP/PAP in peritumoral pancreas. Therefore, we concluded that the use of apparently normal pancreatic regions (not significantly accumu-
lating [18F]FEDL) would be unreliable. In contrast, muscle tissue does not express HIP/PAP and was used as a reference tissue for the Logan graphical analysis. The calculated binding potential of [18F]FEDL in peritumoral pancreatic tissue using muscle as the reference tissue was 2.57 $\pm$ 0.60, which was 20-fold higher than in the pancreas of sham-operated control animals.

No significant accumulation of [18F]FEDL-derived radioactivity was detected in the skeletal structures up to 60 min post injection of [18F]FEDL, which suggests that the radiotracer was not catabolized or de-fluorinated in vivo. The rapid whole body redistribution and fast renal clearance of [18F]FEDL from circulation make this radiotracer especially suitable for imaging of the abdominal area, specifically of the pancreas and liver. A similar pattern of radioactivity biodistribution was previously reported for [18F]FDL in normal NMRI mice and in transgenic mice expressing $\beta$-galactosidase under the control of a ubiquitous ROSA-26 promoter [12]. The similarity in biodistribution of [18F]FEDL and [18F]FDL is not surprising, because the only difference between these radiotracers is that in the [18F]FEDL, the 2'9-position of glucopyranose moiety is directly labeled with 18F-fluoro group, while in the [18F]FDL, the same 2'-position is derivatized with a 18F-fluoroethyl side chain. The low level of [18F]FEDL-derived radioactivity in the pancreas, spleen, liver and intestines at 60 min post i.v. injection may also enable the detection of hepatocellular carcinomas and cholangial carcinoma as well, because the HIP/HAP in known to be over-expressed by the tumor cells (but not the peritumoral liver) [15,16].

Early detection of small pancreatic tumors will require screening of asymptomatic subjects for pancreatic cancer. Despite the demonstration of feasibility of [18F]FEDL PET imaging as a biomarker for detection of early pancreatic carcinomas in an experimental animal model, this diagnostic imaging approach alone can’t be justified for pancreatic tumor screening. This diagnostic imaging approach, however, could be developed as a

| Tissue            | Average | St.Err. |
|-------------------|---------|---------|
| Blood             | 0.51    | 0.11    |
| Brain             | 0.18    | 0.05    |
| Muscle            | 0.21    | 0.03    |
| Kidney            | 5.14    | 2.47    |
| Liver             | 0.66    | 0.23    |
| Lung              | 0.77    | 0.59    |
| Spleen            | 0.22    | 0.08    |
| Stomach           | 0.20    | 0.12    |
| Intestine         | 0.17    | 0.11    |
| Pancreas          | 0.38    | 0.22    |
| Peritumoral pancreas | 4.04 | 2.06    |

Table 1. Radioactivity concentration (%ID/g) in different organs and tissues measured by PET/CT at 60 min post intravenous administration of [18F]FEDL.
follow-up to other biomarker screening approaches that use readily available bodily fluids and tissues, such as blood, pancreatic juice obtained during endoscopic studies. Several genetic syndromes such as familial pancreatitis, Peutz-Jeghers syndrome, and familial atypical multiple mole melanoma are associated with an increased risk of pancreatic cancer, in addition to mutations in the tumor suppressor gene BRCA2 and several DNA mismatch repair genes [17–21]. Currently, genetic syndromes with a high incidence of pancreatic cancer are being targeted for screening [22,23] using blood proteomic profiling [24], serum biomarkers, such as amyloid A [25], RCAS1 [26], CA 19-9, etc. Translational studies are underway to discover novel molecular biomarkers such as up-regulated genes and over-expressed proteins specific for pancreatic carcinomas that could be detected in serum and pancreatic juice. Among the DNA based biomarkers, K-ras mutations are present in 90% of pancreatic cancer. Therefore, other groups have been developing novel PET imaging agents targeting KRAS oncogene, such as the \(^{[64}]\text{Cu}\)DO3A-PNA-peptide [27]. Both mRNA and protein levels of telomerase reverse transcriptase (hTERT) are significantly elevated in pancreatic juice of almost 90% of patients with pancreatic carcinomas [28,29]. Several other proteins or protein fragments are up-regulated in pancreatic carcinoma cells and can be identified in blood (serum) using two dimensional gel electrophoresis or mass spectrometry or antibody-based methods. Recently, it was demonstrated that MUC1 is upregulated in blood of more than 90% of patients with pancreatic carcinoma [30].

Figure 3. Autoradiography of \(^{[18]}\text{F}\)FEDL distribution after intravenous administration and HIP/PAP expression. (A) H&E stained section and (B) color-coded autoradiographic image of \(^{[18]}\text{F}\)FEDL-derived radioactivity distribution in an adjacent section obtained from the same tissue block including: pancreas, spleen and intestine and a small orthotopic pancreatic carcinoma lesion outlined by the dotted lines (bar: 5 mm) and indicated by the arrows; a blue dotted line outlines the area shown at \(\times 15\) higher magnification in panel (C) IHC of HIP/PAP and (D) autoradiography of \(^{[18]}\text{F}\)FEDL-derived radioactivity distribution. High level of \(^{[18]}\text{F}\)FEDL radioactivity is seen in the peritumoral pancreatic tissue, but not in the tumor lesion. (E) A scatter plot and linear regression analysis of relationship between the magnitude of HIP/PAP expression (IHC densitometry, ROD) and \(^{[18]}\text{F}\)FEDL accumulation in peritumoral pancreatic tissue (autoradiography, PSL/mm\(^2\)); an almost linear relationship is observed \((r = 0.88)\).

doi:10.1371/journal.pone.0007977.g003
MUC-1 antigen is identified in pancreatic carcinomas and precursor lesions, but is not detected in normal pancreas. The overall sensitivity and specificity of ELISA for MUC-1 in serum were 82% and 85%, respectively, which is consistent with previous results. An exciting finding in their study is that 92% of stage I cancer cases were above cutoff value for positive response. A positive correlation was observed for mean concentration of MUC-1 in the serum with stage of disease. The same group has recently developed a bivalent 111In-DOTA-labeled antibody to MUC-1 and reported on successful gamma scintigraphy results in mice bearing s.c. xenografts of pancreatic carcinoma [31]. In the latter study, superior imaging results were obtained using the non-radiolabeled bivalent antibody for pretargeting of a radiolabeled TF-10 hapten peptide.

Serum levels of circulating HIP/PAP are also significantly elevated in pancreatic cancer; the level of HIP/PAP correlates with tumor load, nodal involvement, distant metastasis and short survival [32,33]. HIP/PAP protein was also elevated in pancreatic juice in patients with both pancreatic carcinoma and to the lesser magnitude in chronic pancreatitis and could be used to detect early pancreatic injury [34]. Therefore we suggest that ELISA measurements of serum HIP/HAP and MUC-1 levels could be added to a panel of tests for the routine screening of population to identify individuals at increased risk for the developing pancreatic carcinoma. Then, in HIP/HAP-positive individuals [18F]FEDL PET/CT imaging could be performed to identify the location of potential pancreatic carcinoma. Te [18F]FEDL PET/CT could then be followed by more invasive diagnostic imaging approaches, such as endoscopic sonography and endoscopic retrograde cholangio-pancreatography (ERCP), which have been successfully used to detect precancerous lesions in an autosomal dominant familial pancreatic cancer with high penetrance [22].
In summary, we have demonstrated that early stage pancreatic carcinomas could be detected with PET/CT with \(^{18}F\)FEDL, a radioligand for HIP/PAP, which is selectively over-expressed in peritumoral pancreatic acinar cells. Molecular imaging of tumor-specific biomarkers, such as HIP/PAP, over-expressed in peritumoral reactive pancreatic tissue generates the “lesion size amplification” effect and improves the detectability of small pancreatic tumors that are otherwise poorly detectable by conventional non-invasive imaging modalities. When translated into the clinic, \(^{18}F\)FEDL PET/CT imaging should enable earlier diagnosis of pancreatic carcinomas, guide additional diagnostic procedures, facilitate earlier surgeries and thus improve patients’ survival.

**Materials and Methods**

**Cell Culture and Gene Transduction**

Human pancreatic cancer cells L3.6pl were kindly provided by Prof. Isaiah J. Fidler (UT-MD Anderson, Houston, TX). The L3.6pl cells were stably transduced with a retroviral vector bearing a dual reporter gene, termed GL+, which is a tandem fusion of the green fluorescence protein and firefly luciferase genes. Transduced L3.6pl/GL+ cells were selected by FACS and characterized for fluorescence and bioluminescence properties as previously described [35]. The L3.6pl/GL+ cells were grown in flasks with DMEM/F12, supplemented with 10% fetal bovine serum, penicillin and streptomycin, at 37°C in a humidified atmosphere with 5% CO$_2$. The cells were harvested by trypsinization; after centrifugation of cell suspension at 5000 rpm for 5 min the culture medium was aspirated, and the cell pellet was re-suspended in 10% heat inactivated serum obtained from nu/nu athymic nude mice (Charles River, Wilmington, MA) for orthotopic injection, as described below.

**Orthotopic Pancreatic Tumor Model**

All studies in animals were performed according to protocol approved by the Institutional Animal Care and Use Committee of the UT MD Anderson Cancer Center. Four to six weeks old athymic nude mice (N = 8, nu/nu, Charles River, Wilmington, MA) were anesthetized by isoflurane inhalation (2–2.5% in oxygen) and their temperature kept at 38°C with a heat lamp. The CT imaging parameters were X-ray voltage of 80kVp, anode current of 500 μA, an exposure time of 300–350 milliseconds of each of the 360 rotational step. Dynamic PET imaging studies were acquired during 0–60 minutes after administration of \(^{18}F\)-FEDL (3.7 MBq) intravenously as a slow bolus over 1 min while the animals were positioned inside the gantry of the scanner. Images were reconstructed using two dimensional ordered subsets expectation maximization (OSEM) algorithm. PET and CT image fusion and image analysis were performed using software ASIPro 5.2.4.0 (Siemens Preclinical Solutions, Knoxville, TN).

**Bioluminescence Imaging**

To monitor tumor development, the mice were given a single 150-mg/kg intraperitoneal dose of the D-luciferin (Xenogen,CA) on days 4, 7, and 10 after tumor implantation. Under the gas anesthesia (2% isoflurane in oxygen), the animals were placed into the light-tight chamber of the IVIS200 imaging system (Xenogen Corp., Almeda, CA). Bioluminescence images were acquired using the following parameters: image acquisition time 1–5 sec; binning 2; no filter; f/stop; field view, 10 cm. The signal intensity was quantified as sum of all detected photons within the region of interest per second per cm$^2$ per steradian (ph/s/cm$^2$/sr), using Living Image software (Xenogen Corp., Almeda, CA).

**Radiosynthesis of \(^{18}F\)-FEDL**

Detailed radiosynthesis procedure for \(^{18}F\)-FEDL has been reported by us elsewhere [13]. Briefly, initial radiofluorination reactions were carried out using β-O-D-galactopyranosyl-2,3,4,6-O-tetraacetyl-(1–4)-2'- trifluoromethanesulfanyl-3’,5’-O-dibenzyoyl-l’-O-ethyl-yl]-D-mannopyranose precursor and Bu$_4$N\(^{18}F\)F in anhydrous acetonitrile at 80°C for 20 min to produce \(^{18}F\)-FEDL. The crude product was passed through a silica gel SepPak cartridge and eluted with ethyl acetate. Then, the radiolabeled crude intermediate was purified using preparative HPLC. Then, the solvent was evaporated in vacuo and the radiolabeled intermediate was hydrolyzed with 0.5 M NaOMe in methanol at 80°C for 5 min. The final product was neutralized with 1N HCl. The purity of the \(^{18}F\)-FEDL product was verified by TLC and HPLC.

**PET/CT Imaging**

PET/CT imaging was performed using small animal PET/CT scanner INVEON (Siemens Preclinical Solutions, Knoxville, TN). Pancreatic tumor bearing mice (N = 8) were anesthetized with isoflurane (2% in oxygen) and their temperature kept at 38°C with a heat lamp. The CT imaging parameters were X-ray voltage of 80kVp, anode current of 500 μA, an exposure time of 300–350 milliseconds of each of the 360 rotational step. Dynamic PET imaging studies were acquired during 0–60 minutes after administration of \(^{18}F\)-FEDL (3.7 MBq, in 100 μl of saline) intravenously as a slow bolus over 1 min while the animals were positioned inside the gantry of the scanner. Images were reconstructed using two dimensional ordered subsets expectation maximization (OSEM) algorithm. PET and CT image fusion and image analysis were performed using software ASIPro 5.2.4.0 (Siemens Preclinical Solutions, Knoxville, TN).

**Image Analysis and Quantification of Receptor Binding Potential**

Regional radioactivity concentrations (KBq/cm$^3$ or μCi/cm$^3$) were estimated from the maximum pixel intensities within regions of interest (ROIs) drawn around the tumor or organ on trans-axial slices of the reconstructed image sets. The radioactivity uptake in the peritumoral area of pancreas, in the heart and muscle were converted to percent of injected dose per gram of tissue (%ID/g). Logan graphical analysis [14] of the dynamic ROI data was used to assess the magnitude of \(^{18}F\)-FEDL accumulation in the peritumoral pancreas. The ratio of integrated radioactivity concentration in peritumoral pancreas divided by the radioactivity concentration at given time point tumor uptake was set as the y-axis. The ratio of integrated reference tissue uptake divided tumor uptake was set as the x-axis of a Logan plot. The muscle as reference tissue because it has now HIP/PAP expression, while the possibility of HIP/PAP expression in remote regions of “normal” pancreas could not be excluded a priori. The slope of the linear portion of the log plot was distribution volume ratio (DVR). If metabolite corrected plasma curves are not available, the plasma curve can be replaced with reference region curve C$_r$(t). Then the slope of the linear portion of the lot is DVR:

$$\frac{\int_0^T C_{\text{muscle}}(t) dt}{C_{\text{muscle}}(T)} = \frac{\int_0^T C_{\text{tumor}}(t) dt}{C_{\text{muscle}}(T)} + C$$

(1)
The binding potential (BP) can be calculated as:

$$BP = \frac{DVR}{1}$$

(2)

Quantitative Autoradiography (QAR)

After PET imaging, the animals were sacrificed and pancreases with surrounding organs was rapidly extracted, frozen, and embedded in a mounting medium M1 (Shandon-Lipshaw, Pittsburg, PA). Serial 20 μm thick coronal sections of frozen tissues at were obtained at −13°C using a cryomicrotome (CM3050S, Leica, Germany). Tissue sections were thaw-mounted on poly-A lysine coated glass slides and heat-fixed for 5 min at 65°C on a slide warmer (Fischer Scientific, PA). For QAR, tissue sections were exposed to the phosphor plate (Fujifilm Life Science, Woodbridge, CT) along with set of 20 μm autoradiographic standards of known 18F radioactivity concentration, freshly prepared using calf liver homogenate. Knowing the radioactivity concentration in standards and the injected dose, the autoradiographic images were converted to color-coded parametric images of percent injected dose/g tissue (%ID/g) using MCID Elite image analysis software version 7.0 (Imaging Research Inc., St. Catharines, Ontario, Canada).

For ex vivo QAR, 150 μl of saline containing [18F]-FEDL (240 μCi/15 ml) was gently applied directly onto glass slides containing frozen pancreatic tumor tissue sections with perinormal pancreas, obtained from a separate group of tumor xenograft-bearing animals (not injected i.v. with the radiotracer). The tissue sections were placed in a humidified black box to allow 30 min for development. After development, the phosphor plate image intensity was quantified as units of photo-stimulated luminescence per square mm (PSL/mm²). The intensity of immunostaining for HIP/PAP in corresponding ROIs in adjacent tissue sections was quantified by densitometry and expressed as relative optical density (ROD). The data was plotted against each other and linear regression analysis performed to assess the relationship.

Author Contributions

Conceived and designed the experiments: JGG. Performed the experiments: LGF SB HHY DY UM AP YY AV AS SS WT JGG. Analyzed the data: LGF SB HHY DX AS SS WT JGG. Contributed reagents/materials/analysis tools: DY UM AP YY AV WGB MA CL JGG. Wrote the paper: LGF SB JGG.

Immunohistochemistry for HIP/PAP

The IHC for HIP/PAP was performed both in paraffin-fixed tissue sections and in frozen tissue sections, as required. Frozen sections (20 μm) or paraffin-embedded sections (5 μm thick) were incubated in 3% aqueous H2O2 to block the endogenous peroxidase activity, washed and then incubated in 2% normal horse blocking serum for 60 minutes at room temperature. Thereafter, the sections were incubated with monoclonal anti-mouse Reg II antibody (R&D System Inc., Minneapolis, MN) at 1:50 dilution in Tris-NaCl overnight at 4°C. Then, the sections were incubated with the secondary biotinylated horse anti-mouse IgG, followed by avidin-peroxidase conjugation and 3’3-diaminobenzidine chromophore development steps using Vectorstain ELITE Kit (Vector Laboratories, Burlingame, CA) according the manufacturer’s protocol. The tissue sections were either counterstained with hematoxylin or used without counterstaining for densitometric analysis of the intensity of HIP/PAP immunostaining.

[18F]-FEDL Binding Relative to HIP/PAP Expression

Using MCID Elite software version 7.0 (Imaging Research Inc., St. Catharines, Ontario, Canada), the IHC-stained tissue sections were digitized and co-registered with the corresponding adjacent QAR images. The radioactivity concentration (%ID/g) in QAR images was quantified in ROIs as described above. For ex vivo autoradiography, the phosphor plate image intensity was quantified as units of photo-stimulated luminescence per square mm (PSL/mm²). The intensity of immunostaining for HIP/PAP in corresponding ROIs in adjacent tissue sections was quantified by densitometry and expressed as relative optical density (ROD). The data was plotted against each other and linear regression analysis performed to assess the relationship.
21. Rulyak SJ, Lowenfels AB, Maisonneuve P, Brentnall TA (2003) Risk factors for the development of pancreatic cancer in familial pancreatic cancer kindreds. Gastroenterology 124: 1292–1299.
22. Brentnall TA, Bronner MP, Byrd DR, Haggitt RC, Kimney MB (1999) Early diagnosis and treatment of pancreatic dysplasia in patients with a family history of pancreatic cancer. Ann Intern Med 131: 247–255.
23. Goggins M, Canto M, Hruban R (2000) Can we screen high-risk individuals to detect early pancreatic carcinoma? J Surg Oncol 74: 243–248.
24. Honma K, Hayashiya Y, Uozuki T, Okinaka T, Konage T, et al. (2005) Possible detection of pancreatic cancer by plasma protein profiling. Cancer Res 65: 10615–10622.
25. Yokoi K, Shih LC, Kohayashi R, Koossen J, Havke D, et al. (2005) Serum amyloid A as a tumor marker in sera of nude mice with orthotopic human pancreatic cancer and in plasma of patients with pancreatic cancer. Int J Oncol 27: 1361–1369.
26. Yamaguchi K, Enjoji M, Nakashima M, Nakamuta M, Watanabe T, et al. (2005) Novel serum tumor marker, RCAS1, in pancreatic diseases. World J Gastroenterol 11: 5199–5202.
27. Chakhrabarti A, Zhang K, Aruva MR, Cardi CA, Opitz AW, et al. (2007) Radiohybridization PET imaging of KRAS G12D mRNA expression in human pancreas cancer xenografts with [84Cu]DO3A-peptide nucleic acid-peptide nanoparticles. Cancer Biol Ther 6: 948–956.
28. Ohuchida K, Mizumoto K, Yamada D, Yamauchi H, Konomi H, et al. (2006) Quantitative analysis of human telomerase reverse transcriptase in pancreatic cancer. Clin Cancer Res 12: 2066–2069.
29. Nakashima A, Murakami Y, Uemura K, Hayashidani Y, Sudo T, et al. (2009) Usefulness of human telomerase reverse transcriptase in pancreatic juice as a biomarker of pancreatic malignancy. Pancreas 38: 527–533.
30. Gold DV, Modrak DE, Ying Z, Cardillo TM, Sharkey RM, et al. (2006) New MUC1 serum immunoassay differentiates pancreatic cancer from pancreatitis. J Clin Oncol 24: 252–258.
31. Gold DV, Goldenberg DM, Karacay H, Rossi EA, Chang CH, et al. (2006) A novel bispecific, trivalent antibody construct for targeting pancreatic carcinoma. Cancer Res 66: 4019–4026.
32. Cerwenka H, Aigner R, Bacher H, Werkgartner G, el-Shahrawi A, et al. (2001) Pancreatitis-associated protein (PAP) in patients with pancreatic cancer. Anticancer Res 21: 1471–1474.
33. Xie MJ, Motoo Y, Iovanna JL, Su SR, Ohtsuki K, et al. (2003) Overexpression of pancreatitis-associated protein (PAP) in human pancreatic ductal adenocarcinoma. Dig Dis Sci 48: 439–464.
34. Motoo Y, Watanabe H, Yamauchi Y, Xie MJ, Mouri H, et al. (2001) Pancreatitis-associated protein levels in pancreatic juice from patients with pancreatic diseases. Pancreatology 1: 43–47.
35. Nishii R, Volgin AY, Mavdavi O, Mukhopadhyay U, Pal A, et al. (2008) Evaluation of 2′-deoxy-2′-[(18F]fluoro-5-methyl-1-beta-L–s arabinosfuranosyl)uracil ([18F]-L-FMAU) as a PET imaging agent for cellular proliferation: comparison with [18F]-D-FMAU and [18F]FLT. Eur J Nucl Med Mol Imaging 35: 990–996.
36. Bruns CJ, Harbison MT, Kuniyama H, Eae L, Fidler IJ (1999) In vivo selection and characterization of metastatic variants from human pancreatic adenocarcinoma by using orthotopic implantation in nude mice. Neoplasia 1: 50–62.