Photolytical reactions for light induced biological effectors release: on the road to the phototherapeutic window

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Abstract
The use of caged compounds, defined as photolabile precursors of biological effectors, have proven to be attractive in various fields of biology. Photolytical reactions have been widely used to allow a rapid and efficient concentration jump of various biological effectors within organized biological systems. During the last two decades, the challenge was to overcome the difficulty that only high energy UV light was used to induce photochemical reactions on photoremovable protecting groups (PPGs). Infrared-sensitive PPGs should be able to improve in vivo applications of caged compounds. The present review is focused on recent strategies enabling the use of excitation wavelength inside the photo-therapeutical window (600–1000 nm) to efficiently and specifically cleave a chemical bond.

Keywords Photolysis · Uncaging · Two-photon uncaging · Photon-upconversion · Photopharmacology

Introduction
Photolabile precursors of biological effectors, also called caged compounds or photocaged compounds, are molecules whose activity or function is masked by chemical modification using a photolabile protecting group (PPG) [1–4]. Light excitation of these compounds results in a rapid and specific cleavage of a chemical bond leading to a fast and localized concentration jump of the corresponding biological effectors. This strategy has been successfully used to modify the activities of various biomolecules, including peptides [5], proteins [6, 7], nucleic acids [8, 9], neurotransmitters [10], lipids [11] and many other biological effectors [12] in order to restore their biological functions using light. For biomedical applications, the use of photolytical reactions looks also very attractive for drug release and light controlled drug release has been achieved with PPGs or by using photoactivatable linkers [13, 14]. The major drawback of most of the PPGs relies on the use of UV irradiation for the uncaging process, which is characterized by low penetration depth in living tissues and important phototoxicity. NIR sensitive PPGs are highly sought after, firstly because in the so-called photo-therapeutical window (between 600 and 1000 nm) light scattering is low and there is little competing absorption from cells or tissues endogenous biomolecules, such as hemoglobin, melanin and even water [15]. Secondly, NIR radiation can minimize the photodamage to biological specimens [16]. In the last 20 years, different strategies have been explored to overcome the difficulty that only high energy light can induce photolytical reactions. In this review, the three main strategies for designing photoactivatable molecules or systems leading to efficient photolytical reactions using low energy excitation wavelengths will be discussed, with a particular attention for systems working in the photo-therapeutical window. The Fig. 1 summarizes those three strategies from a photophysical point of view.

One‑photon visible to NIR sensitive PPGs
One‑photon photoinduced reactions using organic PPGs are needed to broadly implement the uncaging strategy for various complex biological applications. The efficiency of a PPG to specifically cleave a chemical bond using classical
one-photon excitation (also called uncaging cross-section) is defined as the product of the molar extinction coefficient ($\varepsilon$) and the quantum yield of photolytical reaction ($\phi_u$). In the following paragraphs, we will describe the recent improvement performed on PPGs in the $\text{O}$-nitrobenzyl (NB), $\text{O}$-nitrophenethyl (NPE), coumarinyl, boron-dipyrromethene (BODIPY) and cyanines series. In particular, the most efficient PPGs using visible to far red excitation wavelengths will be described.

$\text{O}$-Nitrobenzyl based PPGs (see scheme 1a for its photolytical reaction pathway) have been the first used PPGs for biological applications [17, 18] and have been extensively applied to control a large number of biological responses using UV excitation [2] as they can be conjugated to a large number of substrates through an alcohol, amine, phosphate, carbamate, thiol, or carboxylic acid moiety. The optimization of the uncaging efficiency for visible light excitation is extremely challenging since it is difficult to develop efficient red shifted NB PPGs. Indeed, in most cases, NB tailored with extended $\pi$-conjugation shows usually a dramatic drop of the uncaging quantum yield [19]. Recently, several strategies were investigated to induce a bathochromic shift of the NB scaffold absorbance and to allow an efficient photolytic reaction upon one-photon excitation. In 2014, Abe, Katan and Kobayashi developed a dialkyl-dihydronaphthalene NB derivative for the release of glutamate neurotransmitter ($1$ in scheme 4) [20]. This latter compound showed an absorbance maximum around 440 nm and was able to release glutamate with an uncaging efficiency of 60 M$^{-1}$ cm$^{-1}$. In 2016, the group of Ellis-Davies developed a bis-styrylthiophene (BIST) NB derivative with an absorption maximum at 440 nm, and was used to develop a photocleavable caged Ca$^{2+}$ chelator ($2$ in scheme 4) with a high uncaging efficiency of 15,180 M$^{-1}$ cm$^{-1}$ [21].

In 2012, our group succeeded to design efficient PPGs in the $\text{O}$-nitrophenethyl serie (see scheme 1b for its photolytical reaction pathway). Dialkylamino-biphenyl NPE based PPGs were therefore described for the release of the GABA neurotransmitter ($3$ in scheme 4) taking advantage of the dialkylamino group which enables functionalization with oligoethylene glycol/carboxylic acid moieties to improve water solubility [22]. Those compounds showed an absorbance maximum around 397 nm and were able to release GABA with an uncaging efficiency of 1125 M$^{-1}$ cm$^{-1}$. In 2014, Wombacher introduced a NPE based PPG by introducing an alkyne linkage on the dialkylamino-biphenyl platform for the development of caged gibberellic acid ($4$ in scheme 4). This modification led to a PPG with a 413 nm absorbance maximum and an uncaging efficiency of 2500 M$^{-1}$ cm$^{-1}$ [23].

Coumarin-based PPGs (see scheme 1c for the photolytical reaction pathway) have been recently applied to the release of a large number of biological effectors due to ease of synthesis and their rapid photolytical reactions (in the ns range) [24]. This scaffold allows to couple a large number of substrates through a carbonate, carbamate, phosphate, pyridine, or carboxylic acid moiety [25]. In the last seven years, many efforts have been performed to build red shifted

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**Fig. 1** Simplified Jablonski diagrams for one-photon induced, two-photon induced and up-converted assisted photolysis
7-(diethylamino)-4-(hydroxymethyl)coumarin (DEAC) PPGs. Therefore, dipolar Donor–Acceptor π-system and quadripolar Donor-Donor π-system have been developed. In 2013, the group of Jullien synthesized a series of such coumarin scaffolds with electron donating group (OMe/Net₂) at the 7-position and different electron withdrawing groups at 2/3 positions aimed at extending the π-conjugation of the system [26]. In particular, this research group was able to develop a coumarin analog bearing thiocarbonyl group at the 2-position for the uncaging of a non-endogenous Cyclofen-OH gene expression inducer [27]. This caged compound (5 in scheme 4) showed an absorption maximum at 492 nm with an uncaging efficiency of 58 M⁻¹ cm⁻¹. Of note, the empty 3d orbital of the sulfur atom of the thiocarbonyl group is expected to enhance the intramolecular charge transfer (ICT) process leading to an increase in the absorbance maximum of this DEAC analog. In 2013, the Ellis-Davies group also modified the DEAC scaffold and introduced a

Scheme 1 Photolytical mechanism of NB, NPE, coumarinyl, BODIPY, nitroindoline, quinoline and pyridinium based PPGs
vinyl acrylate function in the 3-position leading to the so called DEAC450 chromophore [28]. This red shifted PPGs was used to liberate glutamic acid (6a in scheme 4) and showed an absorbance maximum at 450 nm with an uncaging efficiency of 16,800 M$^{-1}$ cm$^{-1}$. In 2017, the group of Ellis-Davies was able to use this interesting PPG to liberate the GABA neurotransmitter and to effectively reduces the antagonism effect of this later caged-GABA (6b in scheme 4) and showed an absorbance maximum at 450 nm with an uncaging efficiency of 16,800 M$^{-1}$ cm$^{-1}$. In 2016, Katan and Abe groups explored the effect of a Donor–Acceptor system leading to a 7-methoxy-coumarin derivative substituted at the 3 position by an electro withdrawing p-nitrophenyl group, this PPG was able to release benzoic acid (7 in scheme 4) and showed an absorbance maximum at 345 nm with an uncaging efficacy of 2045 M$^{-1}$ cm$^{-1}$ [30]. In 2017, the same group also developed Donor-Donor $\pi$-system, therefore the DEAC PPG was modified by an aminophenyl appendage at the 3-position (8 in scheme 4) leading to PPG with an absorption maximum at 407 nm and an uncaging efficiency of 4560 M$^{-1}$ cm$^{-1}$ [31]. In 2018, Zhu’s group synthesized DEAC analogues with electron rich styryl appendages in 3-position [32] inducing red shifted absorption maxima at 446 and 515 nm, and uncaging efficiencies up to 8200 and 17,500 M$^{-1}$ cm$^{-1}$ for 9 and 10 respectively (scheme 4). Of note, the styryl appendage also allowed to produce an unconjugated by-product through an intramolecular reaction on the light generated carbocation (see Scheme 2). This nice improvement lead to the disappearance of the competitive absorption by the photolysis sub-products (sub-product photobleaching). In 2019, the group of Kele introduced modified DEAC PPGs with pyridinium and benzothiazolium heterocycles in 3-position. Compound 11, 12 and 13 showed absorption maxima at 482, 493 and 538 nm respectively with uncaging efficiencies of 260, 335 and 57 M$^{-1}$ cm$^{-1}$ respectively [33]. The same year, the group of Blanchard-Desce also appended Donor–Acceptor $\pi$-system at the 3-position of the DEAC PPGs in order to develop caged glycines. The incorporation of respectively a vinylthiazole (14 in scheme 4), a 2-vinylbenzo[d]thiazole (15a in scheme 4), an elongated fluorenyl-2-vinylbenzo[d] thiazole (15b in scheme 4), a 2-vinylbenzo[d]oxazole (16 in scheme 4) and a 4-vinylbenzo[c][1,2,5]thiadiazole group (17 in scheme 4) led to absorption maxima at 457, 472, 458, 467 and 472 nm respectively and uncaging efficiencies of 7800, 4000, 18,900, 4500 M$^{-1}$ cm$^{-1}$ and below of 600 M$^{-1}$ cm$^{-1}$ respectively [34].

C4′-dialkylamine-substituted variants of the heptamethine cyanine (see scheme 3 for photolytical reaction pathway) have been reported in 2014, as PPGs by the group of Schnerrmann [35]. They demonstrated that cyanine derivatives like compound 18 are able to perform light assisted chemical bond cleavage via a regioselective photooxidative polyene reaction using a 690 nm excitation wavelength. This scaffold was used in combination with a self-immolative linker to uncage a non-endogenous Cyclofen-OH gene expression inducer.

The same year, Urano’s group discovered that the well-known BODIPY fluorophore could be used as a PPG and postulate that the bound cleavage was triggered by a photoinduced electron transfer (PeT)-based process [36]. Classical BODIPYs have an absorption maximum at 502 nm and photocleavage enables the release of phenol function with an uncaging efficiency below to 60 M$^{-1}$ cm$^{-1}$. This research group developed caged histamine using a BODIPY PPG (19). In 2015, further studies were described on a meso-methyl-hydroxy-BODIPY (see scheme 1d for photolytical reaction pathway) connected either directly or via a carbamate linker to biological effectors. First, the group of Weinstain developed a caged- p-nitrobenzylamine (20a), a caged-histamine (20b) and a caged dopamine (20c) using a meso-methyl-hydroxy-BODIPY. Compound 20a showed an

Scheme 2 Styril moiety effect on the photolysis mechanism of position 3 modified coumarinyl PPGs
absorbance maximum at 545 nm and an uncaging efficiency of 7 M\(^{-1}\) cm\(^{-1}\) [37]. Secondly, the group of Winter was able to photorelease acetic acid using the BODIPY derivative 21, and this latter compound showed an absorption maximum at 553 nm with an uncaging efficiency of 117 M\(^{-1}\) cm\(^{-1}\) [38]. In 2017, Klán, Weinstain and Winter groups were able to dramatically increase BODIPY’s uncaging efficiencies by systematic structure-activity relationship studies [39]. In particular, they demonstrated that iodo-BODIPYs are able to increase the uncaging quantum yield and they introduced the BODIPY caged phenylalanine analog 22. This latter showed an absorption maximum at 537 nm with an uncaging efficiency of 20,150 M\(^{-1}\) cm\(^{-1}\). In 2018, the group of Winter added strong electron-donating groups to a meso-methylhydroxy-BODIPY. This red shifted BODIPY derivative was chemically modified by two styryl linkers and benzyl alcohol was used as leaving group via a carbonate linkage. The authors were able to demonstrate that the caged benzyl alcohol 23 had an absorbance maximum at 693 nm with an uncaging efficiency of 73 M\(^{-1}\) cm\(^{-1}\) [40]. BODIPY PPGs exhibit very interesting absorbance wavelengths that now fall in the transparency window enabling more sophisticated biological applications of the uncaging concept. However, the uncaging efficiency need to be improved. Some recent work performed by the group of Peifer, has also pointed out that the uncaging mechanism and his efficiency can be limited in an aqueous environment due to a competitive production of singlet oxygen upon irradiation [41].

Exciting recent progress, particularly using the Coumarinyl, the BODIPY and the cyanine scaffolds, has extended the uncaging concept in wavelengths well into the visible range, but other strategies are still needed to efficiently cleave a chemical bound in the 650–1000 nm region.

**Efficient two-photon sensitive NIR PPGs**

In order to overcome the difficulty that only high energy light can efficiently induce a photolytical reaction, a second strategy based on the use of two-photon induced photolysis was developed during the last 20 years (Fig. 1 center). After the first report of two-photon uncaging by the group of Tsien in 1999 [42], this technique has become well established over the last years as an alternative to classical one-photon excitation for triggering PPGs photolysis [43–45]. In Two-Photon Excitation (TPE), a chromophore will not reach an excited state by absorption of one photon with the energy \(E = \hbar \nu\), but by the simultaneous absorption (within < 1 fs) of two photons of half the energy \(E' = \hbar \nu / 2\) (Fig. 1b). After excitation, it is assumed that the chromophore, i.e. the PPG, undergoes the same photolytic steps as with conventional one-photon excitation [43–46]. TPE is based on a non-linear process, and the probability for TPE to occur scales with the squared light intensity. Due to this quadratic dependency, the excitation will be possible only with very high light intensities, out of range of classical sources used for one-photon excitation. This technique indeed requires the use of pulsed (fs range with high peak power in the range of 10\(^8\) W cm\(^{-2}\)) focalized lasers, inducing a temporal and spatial concentration of photons reaching the molecules. As a consequence, TPE and can only occur in a very small 3D
Scheme 4  Chemical structures of one-photon (or TP) sensitive PPGs
volume surrounding the focal point of the optical system. This volume can be as small as 1 μm³ for a tightly focused laser and no excitation occurs outside the focal volume, in contrast to a single photon process were all the light pathway is excited.

The efficiency of a PPG to specifically cleave a chemical bond using two-photon excitation (δu) is defined as the product of the two-photon absorption cross section (δa expressed in GM) and the uncaging quantum yield of photolytical reaction (ϕu). In 2001, the first biological application of TP uncaging was reported by Kasai and co-workers using 24 4-Methoxy-7-NitroIndolinyl or MNI caged glutamate (see scheme 1e for photolytical reaction pathway) (δu = 0.06 GM at 730 nm). In particular, they were able to mimic a neurotransmitter’s release at single synapse resolution using 730 nm TPE [47]. This work initiated the development of specific PPGs with larger molecular two-photon cross-sections.

Since the two-photon absorption cross-section of a chromophore relies mostly on its molecular structure as well as its environment, many efficient UVA or blue light sensitive PPGs have therefore been embedded within conjugated di-polar, quadrupolar or octopolar architectures in order to improve their two-photon absorption properties for 720–950 nm excitations (Scheme 5) [43–45].

In this context, our group developed a new generation of PPGs for the release of carboxylic acids with TP uncaging efficiencies up to 11 GM. Compounds of this new generation have been successfully applied to the photo-controlled release of the neurotransmitters L-glutamate [48] and GABA [22] in intact neuronal tissue at respectively 720 nm and 800 nm using 25 and 3. Starting from these contributions we will focus on the developments in the field of TP uncaging from the last eight years.

The extension of the aromatic system is one of the rational ways to upgrade two-photon properties of a compound. This was remarkably performed in 2014, by Abe, Katan and Kobayashi groups, using a dialkyl-dihydro naphthalene NB derivative for the release of the Glutamate neurotransmitter 1 who showed an important TP uncaging action cross-section of ~1.2 GM at 680 nm [20]. The same groups were able in 2016 to develop two caged calcium chelator (26a, 26b and 27) (see scheme 5) with respectively an TP uncaging action cross-section of ~1.2 GM at 680 nm [20]. The same groups were able in 2016 to develop two caged calcium chelator (26a, 26b and 27) (see scheme 5) with respectively an TP uncaging action cross-section of ~1.2 GM at 680 nm [20]. The same year, the group of Ellis-Davies reported the BIST-NB caged Ca²⁺ chelator (2) who showed an impressive TP uncaging action cross-section of ~80 GM at 775 nm [21].

The two-photon sensitivity of Quinoline PPGs (see scheme 1f for its photolytical reaction pathway) have also been increased in 2014 by the group of Dalko. New quadrupolar species, where two quinolines moieties were directly linked in two different positions, have led to caged acetic acids 28 and 29 reaching respectively δu = 0.07 GM and 0.40 GM at 730 nm [51]. In 2015, the group of Dalko reached a TP uncaging cross-section of δu = 2 GM at 730 nm for compounds 30 by identifying the C5-substituted isomer as a privileged isomer to increase the two-photon sensitivity of 8-dimethylaminoquinoline derivatives [52]. In 2017, the group of Dalko reported two multipolar Quinoline PPGs with δu values respectively of 0.3 GM at 730 nm and 2.3 GM at 730 nm and for compounds 31 [53] and 32 [54]. In 2020, the group of Dore reexplored the 8-cyano-7-hydroxyquinolin-2-ylmethyl (CyHQ) PPG [55] by introducing several electron withdrawing or donating groups at the C4 position. Compounds 33 a–f were used to mediate an efficient release of homopiperonylic acid with remarkable δu values (up to 2.64 GM) and excellent one photon quantum yields (up to 0.88) [56].

Coumarinyl PPGs have also been extensively optimized to upgrade their two-photon properties. In 2013, the Ellis-Davies reported the DEAC450 PPGs with a TP uncaging action cross-section of 0.5 GM at 900 nm [28]. Katan and Abe groups reported a 7-methoxycoumarin and DEAC analogs modified respectively with an nitrophenyl or a aminophenyl appendage at the 3-position (7 and 8). This modification led to a TP uncaging action cross-section of respectively 3.4 GM at 710 nm [29] and 1.1 GM at 750 nm [30]. In 2018, the Zhu group synthesized the DEAC analogue 9 with electron rich styryl appendages at the 3-position [31]; this latter PPG showed a TP uncaging action cross-section of 39.6 GM at 730 nm. Finally, Kele [32] and Blanchard-Desce [33] groups introduced, in 2019, various donor systems at the 3-position of the DEAC PPGs leading to Coumarinyl PPGs with TP uncaging action cross-section summarized in Table 1. In particular, the caged compound 15b showed an unprecedented uncaging action cross-section of 442 GM at 730 nm!

In summary, the increase of the two-photon absorption sensitivity by molecular engineering led to highly efficient TP sensitive PPGs (up to 440 GM uncaging cross-section for compound 15b). However, it is extremely difficult to predict how this strategy will influence the uncaging quantum yield [19, 57]. Therefore, a second strategy was described for the rational design of TP sensitive PPGs. This strategy called sensitized uncaging, is based on the use of TP sensitive moieties as an antenna to transfer the light energy to a PPG. It has been reviewed, in 2019, by the group of Blanchard-Desce [58]; therefore in this review we decide to present only the most efficient systems. In 2013, a very efficient 2P sensitive modular system was described by Anderson and Blanchard-Desce groups. A pyridinium based PPG (see scheme 1g for its photolytical reaction pathway) able to liberate carboxylic acid functions by photoinduced electron transfer (PeT) was coupled to a symmetric banana-shaped bis-ethynylfluorene (BEF)
Scheme 5  Chemical structures of TP sensitive PPGs
Table 1 Photophysical and photochemical properties of recently developed caged compounds

| Compound | $\lambda_{\text{max}}$/nm | $\phi_u$ | Single photon Uncaging efficiency at $\lambda_{\text{max}}$ M$^{-1}$ cm$^{-1}$ | Two-photon Uncaging efficiency at ($\lambda$/nm) | Solvent |
|----------|-----------------|--------|---------------------------------|---------------------------------|--------|
| 1        | 440             | 0.01   | 60                              | $\sim 1.2$ (680)               | MeOH   |
| 2        | 440             | 0.23   | 15,180                          | $\sim 80$ (775)                | DMSO   |
| 3        | 397             | 0.15   | 1125                            | 11 (800)                       | PBS    |
| 4        | 400             | 0.22   | 2500                            | 20 (800)                       | PBS/DMSO 19/1 |
| 5        | 469             | 0.005  | 135                             | –                              | ACN/Tris 1/1 |
| 6a       | 450             | 0.39   | 16,800                          | 0.5 (900)                      | PBS    |
| 6b       | 450             | 0.23   | $\sim 9900$                     | 0.5 (900)                      | HEPES buffer |
| 7        | 345             | 0.09   | 2045                            | 3.4 (710)                      | DMSO   |
| 8        | 407             | 0.16   | 4560                            | 1.1 (750)                      | DMSO   |
| 9        | 446             | 0.2    | 8200                            | 39.6 (730)                     | MeOH/H$_2$O 9/1 |
| 10       | 515             | 0.7    | 17,500                          | –                              | MeOH/H$_2$O 9/1 |
| 11       | 482             | 0.0088 | 260                             | 1.54 (740)                     | MeOH (1-photon) |
| 12       | 493             | 0.0109 | 335                             | 3.17 (750)                     | MeOH (1-photon) |
| 13       | 538             | 0.0014 | 57                              | 1.83 (740)                     | MeOH (1-photon) |
| 14       | 457             | 0.2    | 7800                            | 32 (950)                       | CD$_3$CN/D$_2$O 9/1 |
| 15a      | 472             | 0.08   | 4000                            | 30 (970)                       | CD$_3$CN/D$_2$O 9/1 |
| 15b      | 458             | 0.45   | 18,900                          | 64 (940)                       | CD$_3$CN/D$_2$O 9/1 |
| 16       | 467             | 0.09   | 4500                            | 25 (970)                       | CD$_3$CN/D$_2$O 9/1 |
| 17       | 472             | <0.02  | <600                            | –                              | CD$_3$CN/D$_2$O 9/1 |
| 18       | 690             | –      | –                               | –                              | –      |
| 19       | 502             | <0.0007| <60                             | –                              | CH$_2$Cl$_2$/MeOH 1/1 |
| 20a      | 545             | 0.00018| 7                               | –                              | PBS/ACN 19/1 |
| 21       | 553             | 0.00238| 117                             | –                              | MeOH   |
| 22       | 537             | 0.32   | 20,150                          | –                              | MeOH   |
| 23       | 693             | 0.0014 | 73                              | –                              | MeOH   |
| 24       | 330             | 0.085  | 360                             | 0.06 (730)                     | PBS    |
| 25       | 317             | 0.09   | 890                             | 3.2 (740)                      | PBS    |
| 26a      | 364             | 0.3    | 3600                            | 16 (740)                       | DMSO   |
| 26b      | 365             | 0.3    | 5630                            | 20.7 (740)                     | C$_6$D$_5$ |
| 27       | 403             | ~0.05  | ~440                            | 7.8 (800)                      | C$_6$D$_6$ |
| 28       | 341             | 0.093  | 305                             | 0.07 (730)                     | ACN/Tris: 1/1 |
| 29       | 353             | 0.066  | 180                             | 0.4 (730)                      | ACN/Tris: 1/1 |
| 30       | 343             | 0.14   | 280                             | 2 (730)                        | ACN/Tris: 1/1 |
| 31       | 380             | 0.015  | 193                             | 0.3 (730)                      | ACN/Tris: 1/1 |
| 32       | 321             | 0.015  | 382                             | 2.3 (730)                      | –      |
| 33a      | 367             | 0.88   | 3500                            | 1.84 (740)                     | KMOPS pH 7.2/CH$_3$CN: 8/2 |
| 33b      | 373             | 0.74   | ~5000                           | 2.25 (740)                     | KMOPS pH 7.2/CH$_3$CN: 8/2 |
(in which the core is extended with substituted anilines via acetylene bridges) TP antenna dye. This complex system led to the synthesis of the caged GABA 34, which showed an important TP uncaging cross-section of 10 GM at 710 nm [59]. In 2016, the group of Blanchard–Desce was able to increase the TP sensitivity of the MNI PPG using a tandem system which a TP absorbing module linked to the PPG via a phosphorous clip, that act together by Forster resonance energy transfer (FRET). This strategy led to a caged acetic acid 35 with a TP uncaging cross-section of 20 GM at 710 nm [60].

Many PPGs have been reported with increased TP uncaging efficiencies by several organic chemistry groups leading to TP uncaging efficiencies up to 440 GM. However, for biomedical applications two-photon absorption is a time-consuming spot-by-spot process to expose macroscopic materials like tissues or organs [3]. These features have recently stimulated the needs of in situ nanotransducers that can generate UV or visible light with a low-energy NIR excitation.

### NIR upconversion assisted photolysis

NIR to UV (or visible) upconversion (UC) processes have been recently used to assist photolytical reactions. The UC process has been established since the 1960s to generate anti-Stokes shift luminescence [61]. This process relies on the existence of multiple intermediate states to accumulate low-energy excitation photons. Those systems are able to absorb energies from two or more photons subsequently and to generate one emission photon with higher energy. This latter emission can be transferred to a PPG in order to induce a photolytically reaction using low energy excitation (Far red or NIR excitation). UC process can take place in organic and inorganic materials and many high brightness upconversion systems have been reported in nanomaterials [62]. The process of UC is mediated by real electronic states, while in TP excitation real intermediate electronic states do not take part. Due to this difference, the TP excitation based on simultaneous interaction of two photons require 5–10 orders of magnitude higher excitation powers but yield more than 5 orders of magnitude lower quantum efficiency in comparison to UC [63]. The intermediate states involved in UC must be excited, therefore material systems where these states have relatively long lifetimes will increase the probability of interaction with subsequent photons. This condition is met by quantum systems with parity-forbidden, but partly allowed optical transitions. Therefore lanthanide (Ln) doped materials are most frequently investigated in the context of UC [64, 65].

In 2010, the group of Branda was able to spectroscopically demonstrate that UC assisted photolysis can be performed on a 3',5'-dialkoxybenzoin PPG using a core–shell lanthanide-doped NaYF4:TmYb nano-particles and an 980 nm excitation (550 W cm−2) [66].

In 2012, Lin and Xing groups, have successfully been able to perform an UC assisted photolysis of an o-nitrobenzyl caged D-luciferin. In this nice work a Tm/Yb co-doped NaYF4 core-shell nanoparticles that have a reduced surface-quenching effect was selected as the platform for the conjugation of D-luciferin using an NB linker (see Fig. 2c). In vivo bioluminescence experiments on mice were performed and strong bioluminescence signals were detected on mice that were injected with the caged D-luciferin/UC nanoparticles conjugate after 1 h of 980 nm excitation (at 255 W cm−2) [67].

In 2011, Branda and Zhao groups, were able to use NaYF4:TmYb UCNPs inside micelles formed by o-nitrobenzyl caged poly(ethylene oxide)-block-polymethacrylate. An UC assisted photolysis (using 980 nm light) was used to cleave the o-nitrobenzyl groups and to convert the polymethacrylate block into an hydrophilic poly-(methacrylic acid), which shifts the hydrophilic hydrophobic balance toward the destabilization of micelles. This system was therefore able to perform a light induced dissociation of the micelles and the release of co-loaded hydrophobic species leading to a nice NIR controlled drug release NP (see Fig. 2a) [68]. In 2012, the same research groups had described a similar drug release strategy based on NB caged hydrogels. This photosensitive hybrid hydrogel loaded with UCNPs, showed that NIR light (980 nm) can induce a gel–sol transition leading to the release of inactive biomacromolecules entrapped in the hydrogel (see Fig. 2a) [69]. In 2014, Wu and co-worker used UCNPs with a mesoporous silica shell to improve the NIR controlled drug release on NP. A mesoporous silica shell was
used to release an anticancer drug doxorubicin using NIR light. Therefore, Ru PPGs were drafted onto the NP surfaces. The Ru complexes acted as molecular valves, which prevented drug leakage (see Fig. 2b). Upon NIR irradiation, UC assisted photolysis enabled to release the drug which inhibited cancer cells growth. Of note, this system allowed to use a relatively low 980 nm excitation (0.35 W cm$^{-2}$) [70].

In 2013, Zhu and Li were able to release the anticancer drug chlorambucil using a hydrophobic 7-aminocoumarin PPG and a yolk–shell structured NP (coating of the NaLuF$_4$ shell on the NaYF$_4$:Yb,Tm core) after 980 nm excitation (50 mW cm$^{-2}$) in a living animal model [71].

In 2013, Su and Yeh groups, were able to use UC assisted photolysis to activate a caged species in order to control cell targeting groups on UCNPs’ surfaces. A tumor-homing agent folate was modified with an $\alpha$-nitrobenzyl PPG and grafted onto UCNPs. Upon NIR irradiation (980 nm), the UC assisted photolysis allowed folate-conjugated UCNPs to target cancer cells [72] leading to a NIR controlled targeting of the NP. This concept was improved in 2014 by Qu and co-workers who introduced UCNPs grafted with photocleavable NB linker bearing an arginine-glycine-aspartic acid (RGD) bioadhesive ligand. This latter UCNPs has been successfully used to control cell adhesion using a 980 nm light excitation (2–4 W cm$^{-2}$) by UC assisted photolysis on an $\alpha$-nitrobenzyl linker [73].

Several other UC assisted photolytical reaction using Lanthanide ion-doped inorganic crystals have already been described [74–77]; but up to date, all those UCNPs still suffer from high power excitation requirement ($10^2–10^{-1}$ W cm$^{-2}$) and inherently poor UC quantum yields.

Therefore, alternative UC strategies have recently been investigated, particularly using organic chromophore-based systems that achieve efficient triplet-triplet annihilation (TTA)-based UC [78, 79]. Those latter UCNPs should allow to perform efficient photolytical reactions using low power NIR excitations in a near future.

**Conclusion**

Photolabile precursors of biological effectors, also known as caged or photocaged compounds, have been extensively used to induce a fast concentration jump of a biological effector by a specific light induced chemical bound cleavage. However most caged compounds absorb light in the 300–400 nm region. The UV region presents several disadvantages, especially for biological applications: (1) high-energy UV light has very limited tissue penetration due to high optical scattering and strong absorbance by endogenous chromophores; (2) UV lead to sample over-heating, (3) UV can cause phototoxic or photoallergic reactions.

Visible and especially NIR light looks much more interesting, since it is considerably less harmful to biological materials and can penetrate deeper into tissues, opening the door to new applications of the uncaging concept especially in the field of drug delivery. In this review, three strategies leading to photoactivatable molecules or systems with
efficient photolytical reactions using red to NIR excitations have been described.

The first strategy is based on the molecular engineering of PPGs leading to a few PPGs activated directly by light of wavelengths above ~600 nm. In particular Coumarinyl, BODIPY and cyanine scaffolds, have extended the uncaging concept in wavelengths up to 500 nm but the application of this strategy is still limited due to relatively low uncaging efficiencies.

The second strategy is based on the use of two-photon induced photolysis. Several PPGs have been recently developed with extremely efficient TP excitation cross-section for the release of various biological effectors with localized NIR excitation.

Finally, a third strategy, based on the use of indirect photoactivation method was presented. NIR to UV (or visible) upconversion NPs have been recently used to assist photolytical reactions.

We are convinced that all those recent improvements should find significant applications especially in the field of nanomedicine soon [80].

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