INTRODUCTION

The growing availability of genomic DNA sequences enables research on profiles of gene expression, single nucleotide polymorphism (SNP) and their role, molecular diagnostics for cancer etc. In turn, these activities require simultaneous interrogation of a given sample for the presence of different nucleic acid sequences. DNA microarrays, “DNA chips”, emerged as an important method for such parallel analysis (Graves, 1999; Wang, 2000; Lockhart and Winzeler, 2000; Heller, 2002). DNA chips function by parallel hybridization of labelled nucleic acid sequences in the solution, known as targets, to an array of nucleic acid probes bound to a surface. Numerous identical probes are localized at a small area known as “spot” or “probe cell”. The composition of the sample is deduced from the label intensities of the different spots after the hybridization. DNA chips are produced in one of two main formats. In cDNA microarrays, long cDNA targets are physisorbed onto the substrate while in oligonucleotide chips short oligonucleotides are chemically bound to the surface via their terminal groups. Our theoretical considerations address the hybridization behavior, kinetics and thermodynamics, of oligonucleotide microarrays when the targets are much longer than the probes as is typically the case in biology experiments (See for examples: Guo et al., 1994; Prix et al., 2002). In particular, we analyze the consequences of the interactions between the long hybridized targets at the surface (Fig.1).

A growing theory effort aims to clarify the underlying physics of DNA chips with view of assisting in their design and in the analysis of the results. The Langmuir isotherm and the corresponding kinetic scheme provide a natural starting point for the modeling (Chan et al., 1995; Livshits and Mirzabekov, 1996; Vainrub and Pettitt, 2002; Bhanot et al., 2003; Held et al., 2003; Zhang et al., 2003; Halperin et al., 2004a, 2004b) as well as the analysis of the experimental results (Forman et al., 1998; Okahata et al., 1998; Steel et al., 1998; Georgiadis et al., 2000; Nelson et al., 2001; Dai et al., 2002; Kepler et al., 2002; Peterson et al., 2002; Hekstra et al., 2003). Within this model, the probes, irrespective of their hybridization state, do not interact. This assumption is justified when the probe density in the spots is sufficiently low. At higher probe densities interactions are no longer negligible and the Langmuir model requires modifications. As we shall discuss, the necessary modifications depend crucially on the length of the targets as characterized by \( N \), the number of bases or monomers. Importantly, in biology experiments the targets are usually significantly longer than the probes. As a result, each hybridized probe binds a long segment of single stranded nucleic acid formed by the unhybridized part of the target (Fig. 1). This leads to two effects. First, when the tails do not overlap the hybridization at an impenetrable surface incurs an entropic penalty. This reduces the equilibrium constant of hybridization with respect to its bulk value. Second, it is necessary to allow for the crowding of these unhybridized “tails” as the fraction of hybridized probes grows. This crowding gives rise to a polymer brush, a phenomenon that was extensively studied in polymer physics (Milner, 1991; Halperin et al., 1992; Rühe et al., 2004). The theory of polyelectrolyte brushes (Pincus, 1991; Borisov et al., 1991; Rühe et al., 2004), as modified to allow for target-probe interactions and wall effects, enables us to analyze the effects of the crowding on the thermodynamics and kinetics of...
hybridization on DNA chips. In particular, we obtain the hybridization isotherm and the rate equation in the brush regime when the unhybridized tails overlap. As we shall see, the free energy penalty associated with the brush gives rise to distinctive modification of the Langmuir isotherm and kinetics. Importantly, the brush penalty reflects both the electrostatic interactions within the probe layer and the entropic price due to the extension of the crowded chains. It results in slower hybridization and lower attainable hybridization.

Our analysis focuses on oligonucleotide microarrays hybridizing with long targets of single stranded (ss) DNA. For simplicity we limit the discussion to the experimentally attainable case of monodispersed targets and probes, a passivated surface that eliminates physical adsorption of DNA and probes anchored to the surface via short spacer chains. The qualitative features of our results apply however to a wider range of systems. Two hybridization regimes appear, depending on the equilibrium hybridization fraction, $x_{eq}$, as set by the bulk concentration of the target, $c_t$. For low $x_{eq}$, the hybridization isotherm is of the Langmuir form, $x_{eq}/(1-x_{eq}) = c_t K$ where $K$ is the equilibrium constant of the hybridization reaction at the surface. For probes comprising $n \ll N$ bases $K$ at an impenetrable surface is reduced by a factor of $(n/N)^{2/5}$ with respect to the equilibrium constant of the free chains in solution. At higher $x_{eq}$, obtained at higher $c_t$, the effective equilibrium constant is modified because of the brush penalty. The leading correction to the hybridization isotherm is $x_{eq}/(1-x_{eq}) = c_t K \exp[-const'(x_{eq}^{2/3} - x_B^{2/3})]$ where $x_B$ corresponds to the onset of brush formation. The formation of the brush does not affect the denaturation rate constant of the hybridized probe. However, it does lower the hybridization rate constant by a factor of $\exp[-const'(x^{2/3} - x_B^{2/3})]$ where $x$ is the instantaneous hybridization fraction. The proportionality constant scales with $N/\Sigma_0^{2/3}$ where $\Sigma_0$ is the area per probe.

To our knowledge, there has been no direct experimental study of the effects of brush formation on the hybridization isotherms and the hybridization rates. Yet, experimental evidence of brush effects has been reported. Guo et al. (1994) observed that the maximum attainable hybridization fraction is reached at higher $\Sigma_0$ when $N$ increases. Su et al. (2002) reported slower hybridization as $N$ increases at fixed $\Sigma_0$. A similar effect was reported for RNA targets by Dai et al. (2002). Further support for the existence of the brush effect is lent by the widespread use of sample fragmentation to achieve a lower average $N$ (See for example: Rosenow et al., 2001; Affymetrix, 2004).

The practical implications of our analysis concern three issues: the design of DNA chips, the sample preparation and the analysis of the data. The design of DNA chips currently reflects the view that an increase in the oligonucleotide density in a spot should increase the signal intensity and therefore the sensitivity (Pirrung, 2002). Certain limitations of this strategy, due to the increase of the DNA diameter upon hybridization and the resulting steric hindrance, has been long recognized (Southern et al., 1999). In marked distinction, our analysis highlights limitations due to the crowding of the long non-hybridized tails of the targets. Thus, in choosing $\Sigma_0$ it is useful to bear in mind the anticipated $N$ of the sample and its effect on the attainable hybridization. When $\Sigma_0$ is fixed, our analysis provides guidelines for the sample preparation. In particular, the choice of $N$ as determined by the PCR primers or the fragmentation procedure. Concerning data analysis, our discussion identifies possible sources of error when comparing spot intensities of samples with different $N$. These may occur because both the onset of saturation and the hybridization rate vary with $N$. In quantitative terms, our analysis yields two guidelines: Concerning equilibrium hybridization, it leads to a simple relationship between the area per probe, $\Sigma_0$, the number of bases in the probe, $n$, the number of bases in the target, $N$, and the attainable sensitivity as measured by $c_{50}$ i.e., the target concentration resulting in 50% hybridization at the spot. Regarding the kinetics, it yields a simple criterion for the onset of slowdown due to the brush formation.

Experiments using DNA chips involve many control parameters concerning the chip design, the sample preparation and the hybridization conditions. These are outlined in Design of Oligonucleotide Microarray Experiments together with a discussion of the resulting hybridization regimes and the choice of parameters used in our numerical calculations. Our analysis incorporates ingredients from the theory of polymer brushes. These are summarized in Background on Polymer Brushes. This section describes the Flory version of the Alexander model of brushes as applied to terminally anchored polyelectrolytes in aqueous solution of high ionic strength. The model is modified to incorporate the effect of an impenetrable grafting surface. This is important in order to ensure crossover to the mushroom regime, of non-overlapping tails, and to enable comparison of the hybridization constants at the surface and in the bulk. Since the hybridization site is typically situated within the target, each hybridized probe carries two unhybridized tails. The necessary modifications are also discussed. When brush formation is possible, the hybridized targets also interact with neighboring probes. The resulting free energy penalty, within the Flory approximation, is described in Target-Probe Interactions. The free energies associated with the brush and with the target-probe interactions enable us to obtain the equilibrium hybridization isotherms. The derivation is discussed in Brush Effects–Thermodynamics of Hybridization. The hybridization isotherms allow to quantify the sensitivity in terms of the corresponding $c_{50}$. In turn, these yield design guidelines relating the sensitivity to $n$, $N$ and $\Sigma_0$. Assuming, and later checking, that the hybridization rate at the surface is reaction controlled enables us to specify the hybridization and denaturation rate constants in the different regimes. The necessary background, on the hybridization kinetics in the bulk and the desorption dynamics out of a brush, as well as the resulting rate equations are discussed in Brush Effects–Kinetics of Hybridization. The
second virial coefficient, \(\nu\), specifying the interactions between the charged monomers of polyelectrolytes in the high salt regime is discussed in Appendix A. Using this \(\nu\), we recover our earlier results of the \(n = N\) case and discuss the comparison to the \(N \gg n\) scenario. In Appendix B we present an alternative derivation of our result for the hybridization constant in the low surface density regime. This utilizes exact results thus avoiding the approximations inherent to the “Alexander-Flory” approximation.

**DESIGN OF OLIGONUCLEOTIDE MICROARRAY EXPERIMENTS**

Oligonucleotide chip experiments vary widely in their design. A brief summary of the possible designs is necessary in order to delineate the range of applicability of our analysis and the different possible regimes. To this end it is helpful to distinguish between three groups of design parameters: The chip design, the sample characteristics and the hybridization conditions. The primary parameters in the chip design (Pirrung, 2002) are the area per probe, \(\Sigma_0\), and the number of bases in the probe, \(n\). \(n\) values in the range 10 to 30 are typical. In this context one should discriminate two approaches to the production of oligonucleotide chips. In one, the probes are synthesized in situ using photolithography. In the other, pre-synthesized oligonucleotides with functionalized end groups are delivered to the spot. In the first approach it is necessary to allow for the production of incomplete sequences leading to polydispersity in \(n\) (Forman et al., 1998). The reported probe densities within spots vary between 1.2 \times 10^{10} and 4 \times 10^{13} probes per cm\(^2\) corresponding to \(2.5 \times 10^2 \text{Å}^2 \leq \Sigma_0 \leq 8.3 \times 10^5 \text{Å}^2\). The chip characteristics also include the nature of the surface treatment used to minimize non-specific adsorption and of the spacer chains joining the probe to the anchoring functionality (length, charge, hydrophobicity, etc.).

A key qualitative characteristic of the sample is the chemical nature of the targets (Graves, 1999; Lockhart and Winzeler, 2000; Heller, 2002). To begin, it is necessary to distinguish between DNA and RNA targets which differ in two respects: First, single stranded (ss) RNA exhibits pronounced secondary structure (loops, hairpins, etc.) which is largely absent in ssDNA. Second, the hybridization free energy of RNA-DNA complexes is higher than that of DNA-DNA ones. For DNA samples, it is further necessary to distinguish between samples of double stranded (ds) DNA, as obtained from symmetric PCR amplification, and ssDNA samples as obtained, for example, using Lambda exonuclease digestion. The hybridization isotherms of the two types of samples are different (Halperin et al., 2004a). The labelling of the targets can also affect the hybridization behavior (Naeef and Magnasco, 2003). Our discussion concerns samples of ssDNA targets assuming ideal labels that do not interfere with the hybridization. It focuses on the role of two quantitative characteristics of the sample: the number of bases in the target, \(N\), and the molar concentration of the target, \(c_t\). \(N\) is determined by the choice of primers used for the PCR amplification or by the fragmentation step in the sample preparation. Note that the products of the PCR are monodisperse while the fragmentation introduces polydispersity in the size of the targets. In this last case it is only possible to control the average size of the targets. Typical reported values for PCR products vary in the range 100 \(\leq N \leq 350\). The average \(N\) resulting from the fragmentation procedure is not always specified but the range 50 \(\leq N \leq 200\) is representative. It is useful to note another distinction between the two procedures. Targets produced by PCR often have the hybridization site situated roughly in the middle of the target. In the case of fragmented targets, the location of the hybridization site is no longer controlled. With regard to \(c_t\) it is helpful to stress the distinction between bioanalytic experiments, utilizing DNA chips to interrogate biological samples (See for example: Prix et al., 2003), and physical chemistry experiments aiming to understand the function of DNA chips (See for example: Peterson et al., 2002). In biology experiments \(c_t\) is a priori unknown since it is set by the biological sample and its treatment. In marked contrast, in physical chemistry experiments the target concentration is imposed by the experimentalist as it is the composition of the sample. In such experiments the target used is often identical in length to the probes, \(n = N\). As noted earlier, our analysis is motivated by bioanalytical experiments where \(N \gg n\).

The hybridization conditions include the composition of the hybridization solution, the hybridization temperature, \(T\), and the hybridization time, \(t_h\). Typical hybridization temperatures vary over the range 30°C \(\leq T \leq 60°C\) depending on \(n\) and the GC fraction. The hybridization times also vary widely with typical values in the range of \(2h \leq t_h \leq 16h\). In most cases the hybridization solution contains 1M of NaCl.

Different hybridization regimes are possible, depending on the values of \(n\), \(N\) and \(\Sigma_0\). To distinguish these regimes, it is necessary to first specify the molecular length scales of ssDNA and dsDNA. These are well established for dsDNA (Cantor and Schimmel, 1980). In the range of parameters considered, dsDNA is a rod-like molecule with each base pair contributing 3.4Å to its length. The radius of dsDNA is 9.5Å and its cross section area is 284Å\(^2\). We will limit our analysis to \(\Sigma_0 > 284\text{Å}^2\) in order to avoid discussion of steric hindrance to hybridization. The corresponding characteristics of ssDNA are not well established. A typical value of the monomer size is \(a = 6.6\) Å (Smith et al., 1996; Strick et al., 2003). The cited values of the persistence length, \(l_p\), vary between \(l_p = 7.5\) Å and \(l_p = 35\) Å (Mills et al., 1999). ssDNA is often described as a random coil though long range interactions are expected to give rise to swollen configurations (Turner, 2000). In the following we will consider ssDNA as a swollen coil characterized by its
Flory radius (Rubinstein and Colby, 2003). This choice is dictated by our treatment of the brush, where the Flory radius emerges as a natural length scale. Accordingly, an isolated unhybridized probe occupies a hemisphere of radius \( r_F \sim n^{3/5}a \) while a terminally hybridized target occupies a hemisphere of radius \( R_F \sim (N - n)^{3/5}a \approx N^{3/5}a \). As we shall discuss, the unhybridized probes do not interact when \( r_F^2 < \Sigma_0 \). Similarly, when \( R_F^2 < \Sigma_0 \) there is no brush regime. It is thus possible to distinguish between three different scenarios. A Langmuir regime is expected when \( \Sigma_0 > R_F^2 > r_F^2 \). Brush effects, with no interactions between the probes, will occur when \( r_F^2 < \Sigma_0 < R_F^2 \). Finally, when \( \Sigma_0 < r_F^2 < R_F^2 \) both the brush effect and probe-probe interactions play a role. All three scenarios occur in the reported variety of DNA chips.

In the following we consider the role of \( n \), \( N \) and \( \Sigma_0 \) in bioanalytical experiments. For brevity we focus on the simplest among the experimentally realistic situations. Thus, we consider monodispersed ssDNA targets and monodispersed oligonucleotide probes. This avoids complication due to unspecified polydispersity and to competitive bulk hybridization. It is convenient to concentrate on the simplest among the experimentally realistic situations. Thus, we consider monodispersed ssDNA targets and ssDNA were investigated, the area per probe was varied in the range 300 \( \AA^2 \leq \Sigma_0 \leq 3000 \AA^2 \) and the hybridization was carried out at \( T = 30^\circ \text{C} \). The hybridization times varied with \( N \) being \( t_h = 2 - 3h \) for \( N = 157 \) and \( t_h = 6 - 8h \) for \( N = 347 \). Note that in this study some of the data corresponds to the \( \Sigma_0 < r_F^2 < R_F^2 \) regime where probe-probe interactions are not negligible. The second system is the Affymetrix GeneChip E. Coli Antisense Genome Array (Affymetrix, 2004). In this case, probes of length \( n = 25 \) hybridize with fragmented, thus polydispersed, ds cDNA targets with average length in the range 50 \( \leq N \leq 200 \). The hybridization is carried out at \( T = 45^\circ \text{C} \) for \( t_h = 16h \). A rough approximation of \( \Sigma_0 \) for Affymetrix chips was obtained from the estimated density of functional

Our analysis is concerned with the modifications of the hybridization isotherm and rate equations as \( \Sigma_0 \) decreases from the Langmuir range, \( \Sigma_0 > R_F^2 > r_F^2 \), into the brush regime, \( r_F^2 < \Sigma_0 < R_F^2 \). To implement this program, it is helpful to identify a reference state. In the following we utilize a probe layer that approaches the bulk values for the hybridization rate and equilibrium constants. We argue that this is the case when the following conditions are satisfied. First, the surface is perfectly non-adsorbing to both ss and ds DNA. Under these conditions adsorbed states are not involved in the hybridization reaction and the two state approximation for the hybridization reaction is justified. Second, the probes are attached to the surface via long, flexible and neutral spacers. We argue that the effect of the surface diminishes as the length of the spacers increases. Note that the spacers modify two effects. One is the steric hindrance that occurs when the probes are directly attached to the surface. The other is the reduction in the number of accessible configurations in the vicinity of an impenetrable planar surface. Ideally, the reference state involves spacer chains that do not interact with either the probes and the targets. The third condition is that the distance between the anchored probes ensures zero probe-probe interaction energy, irrespective of their hybridization state. For this reference state, the equilibrium hybridization constant at the surface \( K_{pt} \) approaches \( K_{pl} \), the equilibrium hybridization constant for the bulk reaction between the free chains. Accordingly, the hybridization isotherm in the small spot limit, when the hybridization at the surface has a negligible effect on initial molar concentration of the target \( c_t \), is

\[
\frac{x_{eq}}{1 - x_{eq}} = K_{pt}c_t. \tag{1}
\]

It is important to distinguish between \( K_{pt} \) and \( K_{pl}^0 \)

\[
K_{pl}^0 = \exp \left( -\frac{\Delta G_{pl}^0}{RT} \right), \tag{2}
\]

where \( \Delta G_{pl}^0 \) is the molar standard hybridization free energy as obtained from the nearest neighbor model (SantaLucia and Hicks, 2004), \( T \) is the temperature and \( R = 1.987 \text{cal.mol}^{-1}.K^{-1} \) is the gas constant. First, \( K_{pt}^0 \) and \( \Delta G_{pl}^0 \) as calculated from the nearest neighbor model are identical for all \( N \geq n + 2 \). They allow, at most, for the effect of two dangling ends. Second, this model incorporates only nearest neighbor interactions along the backbone of the chain. It thus assumes that the oligonucleotide adopts the configuration of an ideal random coil. In particular, \( \Delta G_{pt}^0 \) does not account for excluded volume interactions between the monomers. In addition, \( \Delta G_{pt}^0 \) clearly does not allow for the effect of the impenetrable wall or for the interactions between the hybridized targets or between them and the neighboring probes. These additional terms and their effect on the hybridization isotherm will be discussed in the following three sections.

Our choice of the parameters used in the numerical calculations is based on two experimental systems. One, of Guo et al. (1994), utilized probes of length \( n = 15 \) with PCR produced targets of length \( N = 157 \) or 347. Both ssDNA and dsDNA were investigated, the area per probe was varied in the range 300 \( \AA^2 \leq \Sigma_0 \leq 3000 \AA^2 \) and the hybridization was carried out at \( T = 30^\circ \text{C} \). The hybridization times varied with \( N \) being \( t_h = 2 - 3h \) for \( N = 157 \) and \( t_h = 6 - 8h \) for \( N = 347 \). Note that in this study some of the data corresponds to the \( \Sigma_0 < r_F^2 < R_F^2 \) regime where probe-probe interactions are not negligible. The second system is the Affymetrix GeneChip E. Coli Antisense Genome Array (Affymetrix, 2004). In this case, probes of length \( n = 25 \) hybridize with fragmented, thus polydispersed, ds cDNA targets with average length in the range 50 \( \leq N \leq 200 \). The hybridization is carried out at \( T = 45^\circ \text{C} \) for \( t_h = 16h \). A rough approximation of \( \Sigma_0 \) for Affymetrix chips was obtained from the estimated density of functional
FIG. 1: A schematic picture of the hybridization of long targets at a layer of short probes. For simplicity we depict the case of targets with a terminal hybridization site, when each hybridized probe carries a long ssDNA tail. Three regimes occur: a) In the 1 : 1 regime the distance between the probes, $\Sigma_0^{1/2}$, is large and each hybridized target can only interact with its own probe. There is no crowding of the tails. b) In the 1 : $q$ regime the probe density is higher. At low hybridization fraction each target interacts with $q = R_F^2/\Sigma_0$ probes. c) As the hybridization fraction increases the hybridized targets begin to crowd each other thus forming a brush with an area per chain $R_F^2 > \Sigma > \Sigma_0$. Note that in the general case the hybridization site is situated roughly in the middle of the target and each hybridized probe carries two tails (a).

Table 1: The thermodynamic parameters utilized in the numerical calculations correspond to two probes: (i) The $n = 15$ wild type probe $p1$ (5′ - CGTCTTTTTCAAGAA – 3′) incorporates the codon 406 of exon 4 of the human tyrosinase gene. The $N = 157$ and 347 targets incorporate the perfect complementary segment 5′ - TTCTTTGAGAGGAGC - 3′ (Guo et al., 1994). (ii) The Affymetrix E.Coli Antisense $n = 25$ probe $p2$ annotated AFFX-BioB-5′ at 242.77, with interrogation point 177, corresponds to the sequence 5′ - AGATGCATTACTGTGCCCGCAACGC - 3′. The fragmented cDNA targets incorporate the perfect complementary sequence 5′ - CGTTTGGGCGAGATTTGAAATCT - 3′. The parameters are calculated from the nearest neighbor model (SantaLucia, 1998; Peyret et al., 1999; HyTherTM) using the HyTherTM program with a 1 M NaCl salt concentration. Since the targets are longer than the probes two dangling ends are invoked.

| probe | $\Delta H^0_{pt}$ kcal.mol$^{-1}$ | $\Delta S^0_{pt}$ cal.mol$^{-1}.K^{-1}$ | $\Delta G^0_{pt}(30^\circ C)$ kcal.mol$^{-1}$ | $\Delta G^0_{pt}(45^\circ C)$ kcal.mol$^{-1}$ |
|-------|----------------------------------|--------------------------------------|-----------------------------------------------|-----------------------------------------------|
| p1    | -121.00                          | -334.06                              | -19.73                                        | -14.72                                        |
| p2    | -203.30                          | -546.32                              | -37.69                                        | -29.49                                        |

BACKGROUND ON POLYMER BRUSHES

Polymer brushes are formed by chains with one monomer anchored to a planar surface (Milner, 1991; Halperin et al., 1992). In the simplest case, the anchoring moiety is the terminal monomer. When the area per chain, $\Sigma$, is large the chains do not crowd each other. In this “mushroom” regime, the chains may be roughly considered as occupying hemispheres whose radius is comparable to the Flory radius of the free chain, $R_F$. When the surface density increases such that $\Sigma \leq R_F^2$, the chains begin to crowd each other thus forming a “brush”. In the brush regime the chains stretch out along the normal to the surface so as to decrease the monomer concentration, $c$, and the number of repulsive monomer-monomer contacts. A simple description that captures the leading behavior of brushes is provided by the Alexander model (Alexander, 1977; Milner, 1991; Halperin et al., 1992). Within it the concentration profile of the brush is modeled by a step function of height $H$ for the entropy loss incurred because of the stretching of a Gaussian chain, comprising of $Na/l_p$ persistent sequences of length $l_p$, along the normal to the surface. Here $a$ is the monomer size, $l_p$ is the persistence length of the chain and the span of the Gaussian unswollen coil is $R_0 = \sqrt{Na l_p}$. The last term arises because the impenetrable surface carrying the anchoring site reduces the number of accessible configurations of the tethered chain. For a Gaussian chain with a free end at altitude $H$ the number is reduced by a factor of $H l_p/R_0^2$ (DiMarzio, 1965). This contribution is often ignored because it has a negligible effect on the equilibrium dimensions of the chains. It leads however to a significant modification of the hybridization constant at the surface. The last two terms of Eq.3 apply, in this form,
when $Na \gg l_p$. We have omitted a term allowing for the entropy associated with the placement of the free end. This is because the Alexander model assumes that all free ends are constrained to the brush boundary. For simplicity we ignore, here and in the following, numerical factors of order unity. Minimization of $G$ with respect to $H$ yields the equilibrium values of $G_{\text{brush}}$ and $H$

$$\frac{G_{\text{brush}}}{kT} = N \left( \frac{a^2}{\Sigma} \right)^{2/3} \left( \frac{a}{l_p} \right)^{1/3} \left( \frac{v}{a^3} \right)^{2/3} - \ln \left[ \left( \frac{a^2}{\Sigma} \right)^{1/3} \left( \frac{l_p}{a} \right)^{1/3} \left( \frac{v}{a^3} \right)^{1/3} \right],$$

(4)

$$\frac{H}{a} = N \left( \frac{a^2}{\Sigma} \right)^{1/3} \left( \frac{l_p}{a} \right)^{1/3} \left( \frac{v}{a^3} \right)^{1/3}.$$ 

(5)

In the mushroom regime, the chains occupy a hemisphere of radius

$$\frac{R_F}{a} = N^{3/5} \left( \frac{l_p}{a} \right)^{1/5} \left( \frac{v}{a^3} \right)^{1/5}.$$ 

(6)

Accordingly, the free energy per chain in the mushroom regime, $G_{\text{mush}}$, is set by the requirement $G_{\text{mush}} = G_{\text{brush}}$ at the mushroom-brush boundary when $\Sigma = R_F^2$ and $H = R_F$ thus leading to

$$\frac{G_{\text{mush}}}{kT} = N^{1/5} \left( \frac{a}{l_p} \right)^{3/5} \left( \frac{v}{a^3} \right)^{2/5} - \ln \left[ N^{-2/5} \left( \frac{l_p}{a} \right)^{1/5} \left( \frac{v}{a^3} \right)^{1/5} \right].$$ 

(7)

As noted earlier, the properties of the chains in the mushroom regime are comparable to those of free coils. In turn, the free coil behavior is specified by the free energy (De Gennes, 1979)

$$\frac{G}{kT} = \frac{N^2}{r^3} + \frac{r^2}{Nal_p}$$

(8)

leading, upon minimization with respect to the radius $r$, to $R_F$ as given by Eq.4 and to the equilibrium free energy of a coil

$$\frac{G_{\text{coil}}}{kT} = N^{1/5} \left( \frac{a}{l_p} \right)^{3/5} \left( \frac{v}{a^3} \right)^{2/5}.$$ 

(9)

The difference between $G_{\text{mush}}$ and $G_{\text{coil}}$ is due to the logarithmic correction $-\ln(R_F/Na)$ arising from the wall effect.

Within the approach described above, the nature of the grafted chain is specified by three parameters, the monomer size $a$, the persistence length $l_p$, and the second virial coefficient associated with monomer-monomer interactions $v$. For the case of a brush formed by polyelectrolyte chains in aqueous solution of high ionic strength, “high salt”, $v$ can be approximated by (Pincus, 1991; Appendix A)

$$v = \frac{2\pi}{3} a^3 \left( 1 - \frac{\theta}{T} \right) + 2\pi l_B r_D^2.$$ 

(10)

The first term allows for the hard core repulsion between the monomers and for a weak, long ranged, van der Waals attraction between them. Here $\theta$ is the theta temperature where $v$ of a neutral chain vanishes thus leading to the behavior of an ideal Gaussian coil. This term by itself is used to describe the behavior of neutral polymers (Rubinstein and Colby, 2003). The second term arises from the screened electrostatic interactions between the singly charged monomers. Here $l_B = e^2/\epsilon kT$ is the Bjerrum length (Evans and Wennerström, 1994) where $\epsilon$ is the dielectric constant, $k$ the Boltzmann constant and $T$ the temperature. In water, with $\epsilon \approx 80$ at room temperature, $l_B \approx 7 \text{Å}$. Note that the variation of $\epsilon$ with $T$ contributes to the $T$ dependence of $l_B$. The Debye length $r_D$ characterizes the range of the screened electrostatic interactions in a salt solution (Evans and Wennerström 1994). For a 1 : 1 salt with number concentration of ions $c_s$, $r_D = 1/\sqrt{8\pi l_B c_s}$ thus, in a 1M solution $r_D = 3 \text{Å}$. In our model, the presence of the $2\pi l_B r_D^2$ term in $v$ distinguishes polyelectrolyte brushes from neutral ones. It is important to stress the limitations of approximating $v$ by Eq.10. It corresponds to the interaction between individual charged spherical monomers. For cylindrical non-charged monomers $v \approx l_p^2 a$ rather than $v \approx a^3$ (Rubinstein and Colby, 2003). Furthermore, this description does not allow for the contribution of Hydrogen bonds with water nor for the effect of correlations on the electrostatic interactions. Finally, the appropriate $\theta$ temperature remains to be determined. With these caveats in mind, the second term is roughly comparable to $2\pi a^{3/5}$ and should be dominant for $T \gtrsim \theta$. As a result $v$ is comparable to $2\pi a^{3/5}$ and the swelling behavior of the chain is similar to that of a neutral chain in an athermal
solvent (De Gennes, 1979). In other words, even short chains swell to their Flory radius. We should add that by using \( v \approx 2\pi l_B r_F^2 \) we are able to recover our earlier results (Halperin et al., 2004a) for the case of \( n = N \) (Appendix A).

In the Flory type approach, described above, the equilibrium state is determined by a global balance of the osmotic pressure of the monomers and the restoring elastic force of the stretched Gaussian chains. A more refined analysis of the brushes, utilizing self consistent field (SCF) theory, is possible. This avoids the assumptions of uniform stretching and step-like concentration profiles. It yields the same functional forms for the characteristic height, \( H \), and for \( G_{\text{brush}} \) but with somewhat different numerical prefactors. With these reservations in mind we utilize the simplest approach, described earlier, because it typically yields the correct leading behavior in similar systems. A SCF theory is necessary for the description of effects that depend strongly on the details of the concentration profile and the distribution of the free ends.

Our discussion thus far concerned brushes anchored to the surface by the terminal head group. In DNA chips the situation is often different in that the hybridization site, the anchoring functionality, is located roughly at the middle of the target. As a result, each hybridized probe carries two unhybridized tails (Fig.1d) of length \( N_1 \) and \( N_2 = N_1(1 + \alpha) \) such that \( N_1 + N_2 + n = N \). In considering the effect of this feature note that, in the brush regime, the details of the anchoring functionality are screened with a distance \( \Sigma^{1/2} \) from the surface. As a result, it is possible to estimate the modification of \( G_{\text{brush}} \) and \( H \) in two cases, \( N_1 = N_2 \gg n \) and \( N_2 \gg N_1 \gg n \). When \( N_1 = N_2 \) the resulting brush is similar to that formed by chains of length \( N/2 \) but with an area per chain \( \Sigma/N \). In this case \( G_{\text{brush}} \) is larger by a factor \( 2^{2/3} \approx 1.6 \) while \( H \) is smaller by a factor \( 2^{2/3} \) in comparison to the values found for a brush of terminally anchored chains of length \( N \) and area per chain \( \Sigma \). In the limit of \( N_2 \gg N_1 \gg n \) the resulting brush may be considered as bidispersed, comprising an equal number of chains of length \( N_1 \) and \( N_2 \). Such a bidispersed brush can be described as a superposition of two brushes (Birshtein et al., 1990). A simple two layer model incorporates an inner brush of chains of length \( N_1 \) and area per chain of \( \Sigma/2 \) and an outer brush formed by chains of length \( N_2 - N_1 = \alpha N_1 \) and area per chain \( \Sigma \) at the distal boundary of the inner brush. Within the Flory approximation this scheme leads to \( \tilde{G}_{\text{brush}} = \frac{\alpha N_0}{\alpha + 1} G_{\text{brush}} \) and \( \tilde{H} = \frac{\alpha + 1/2}{\alpha + 2} H \) where \( G_{\text{brush}} \) and \( H \) correspond to a monodispersed brush of chains of length \( N \) with an area per chain \( \Sigma \). Note that \( \alpha = 0 \) corresponds to \( N_1 = N_2 \) while \( \alpha \gg 1 \) to \( N_2 \gg N_1 \). In both cases, the effect is to modify \( G_{\text{brush}} \) and \( H \) as obtained earlier by a multiplicative factor of order unity. In keeping with our policy we will omit these numerical factors in the interest of simplicity.

**TARGET-PROBE INTERACTIONS**

The preceding discussion of brushes allows for the interactions among the hybridized targets and the effects of the impenetrable wall. However, the brush regime is only attainable when the hybridized targets can interact with neighboring probes, thus giving rise to an additional contribution to the free energy of the system. In discussing the target-probe interactions it is useful to distinguish between three regimes. When \( \Sigma_0 > R_F^2 > r_F^2 \) the hybridized targets can not crowd each other. Roughly speaking, each one may be considered to occupy a hemisphere of radius \( R_F \) containing a single probe that is hybridized to the target (Fig.1a). Since each target interacts with a single probe we will refer to this regime as 1 : 1. Our principle interest is in the two regimes that occur when \( \Sigma_0 > N_0 > r_F^2 \) or \( N_0 > \Sigma_0 > r_F^2 \). When the hybridization degree \( x \) is sufficiently small each target will occupy, as before, a hemisphere of radius \( R_F \). However, it will now interact with \( q = R_F^2/\Sigma_0 \) probes (Fig.1b). We will thus refer to this regime as 2 : 1. Note that in the polymer science nomenclature both 1 : 1 and 2 : 1 regimes fall into the “mushroom” range, when the tethered chains do not overlap. The brush threshold occurs at \( x = x_B \) when the hemispheres occupied by the different targets come into grazing contact. For a surface of total area \( A_T \) the area per hybridized target is \( \Sigma = A_T/xN_T = \Sigma_0/x \) where \( N_T \) is the total number of probes. \( x_B \) corresponds to \( \Sigma = R_F^2 \) or \( x_B = \Sigma_0/R_F^2 = 1/q \). When \( x \) exceeds \( x_B \) the hybridized targets begin to overlap thus forming a brush (Fig.1c). Since the area per chain in this regime decreases as \( \Sigma = \Sigma_0/x \) the target experiences interactions only with \( x^{-1} < q \) probes.

To estimate the free energy of interactions between the target and the probes, in the spirit of the Flory approach, we assume that each probe contributes an interaction free energy \( G_{\text{int}}/kT = vmc \). Here \( c \) is the monomer concentration within the monomer cloud formed by the hybridized targets i.e., we assume the interaction with the probes does not affect \( c \) as obtained in our earlier discussion of the mushroom and brush regimes. As we shall elaborate later, this assumption is justified only when \( G_{\text{int}} \ll G_{\text{coil}}(N) \) or

\[
\Sigma_0 \gg N^{1/5} na^2 \left( \frac{l_B}{a} \right)^{2/5} \left( \frac{v}{a^3} \right)^{2/5}.
\]  

(11)

In the 1 : 1 regime each hybridized target occupies a hemisphere of radius \( R_F \) incorporating a single probe. Accordingly
\[ \frac{G_{\text{int}}^{1:1}}{kT} = v n c \] with \( c = N/R_F^3 \) thus leading to

\[ \frac{G_{\text{int}}^{1:1}}{kT} = \frac{n}{N^{3/5}} \left( \frac{a}{l_p} \right)^{3/5} \left( \frac{v}{a^3} \right)^{2/5}. \] (12)

This estimate is reasonable when \( N \gg n \) such that the region occupied by the unhybridized target is sufficiently large so as to encompass the hybridized probe. Roughly speaking, this implies \( (N - n)^{3/5} a > 3.4 n A \). Within the \( 1:q \) regime each hybridized target interacts with \( q = R_F^2 / \Sigma_0 \) probes. Accordingly, \( G_{\text{int}}^{1:q} / kT = v (R_F^2 / \Sigma_0) n c \) with \( c = N/R_F^3 \) or

\[ \frac{G_{\text{int}}^{1:q}}{kT} = N^{2/5} n \left( \frac{a^2}{\Sigma_0} \right) \left( \frac{a}{l_p} \right) \left( \frac{v}{a^3} \right)^{4/5}. \] (13)

\( G_{\text{int}}^{1:1} \) and \( G_{\text{int}}^{1:q} \) are independent of \( x \). In marked contrast \( G_{\text{int}}^{B} \), accounting for the target-probe interactions in the brush regime, varies with \( x \). This variation arises because of the \( x \) dependence of the monomer concentration within the brush, \( c_{\text{brush}} = N / \Sigma H \) where \( \Sigma \sim 1/x \) and \( H \sim x^{1/3} \). \( G_{\text{brush}}(x) \) is obtained from Eq.4 upon replacing \( \Sigma \) by \( \Sigma_0 / x \). Within the Flory approach the total interaction free energy between the targets and the probes is \( v N T n c_{\text{brush}} \). The interaction free energy per hybridized target is thus \( v n c_{\text{brush}} / \Sigma_0 \) or

\[ \frac{G_{\text{int}}^{B}}{kT} = \frac{v n N}{\Sigma_0} H = n x^{-1/3} \left( \frac{a^2}{\Sigma_0} \right)^{2/3} \left( \frac{a}{l_p} \right)^{1/3} \left( \frac{v}{a^3} \right)^{2/3}. \] (14)

The condition Eq.11 ensures that the interaction term \( G_{\text{int}}^{1:q} \) is a weak perturbation to the Flory free energy of the mushroom \( G_{\text{mush}}(N) \). When this requirement is not satisfied the chain span exceeds the Flory radius. This is an unphysical result since the interactions driving the extra swelling are confined to the surface. In this case the chain can no longer be assumed to occupy a hemispherical region encompassing the probes. The uniform monomeric distribution inherent to the Flory approach should be refined so as to reflect locally stretched configurations allowing to avoid the probes. For simplicity we will not consider this regime.

**BRUSH EFFECTS—THERMODYNAMICS OF HYBRIDIZATION**

Having obtained the free energy terms associated with target-target and target-probe interactions at the surface, we are in a position to investigate their effect on the hybridization isotherm. To simplify the equations we set \( v = a^3 \) and \( l_p = a \). The hybridization isotherm is determined by the equilibrium condition of the hybridization reaction \( p + t = pt \) at the probe layer that is \( \mu_{pt} = \mu_p + \mu_t \) where \( \mu_i \) is the chemical potential of species \( i \). Here \( p \) and \( t \) signify single stranded probe and target while \( pt \) is the hybridized probe-target pair. We first consider \( \mu_t \). In practice, the molar concentration of the targets, \( c_t \), is only weakly diminished by the hybridization reaction and it is reasonable to assume that \( c_t \) is constant. The generalization to the opposite case, when this small spot approximation fails, is straightforward (Halperin et al., 2004a). Since the target solution is dilute and the ionic strength of the solution is high, electrostatic interactions between the targets are screened. Consequently \( \mu_t \) assumes the weak solution form

\[ \mu_t = \mu_t^0 + N_{Av} G_{\text{coil}}(N) + RT \ln c_t \] (15)

where \( \mu_t^0 \) is the chemical potential of the standard state of the hybridization site and \( N_{Av} \) is the Avogadro number. We choose a standard state such that \( \mu_{pt}^0 - \mu_p^0 - \mu_t^0 = \Delta G_{pt}^0 \) as given by the nearest neighbor method. As discussed earlier, this implies a standard state having an ideal coil configuration. When the hybridization site is within the target, it also reflects the contribution of two dangling ends. \( G_{\text{coil}}(N) \), as given by Eq.7, allows for the swelling of the free coil due to excluded volume and electrostatic interactions. Strictly speaking, \( \mu_t = \mu_t^0 + N_{Av} G_{\text{coil}} + RT \ln a_t \) where \( a_t \) is the activity (Moore, 1972). The dimensionless \( a_t \) is related to the molar concentration of targets \( c_t \) via \( a_t = \gamma c_t \) where \( \gamma \) is the activity coefficient. Since \( \gamma \rightarrow 1 \) as \( c_t \rightarrow 0 \) we will, for simplicity, express \( \mu_t \) by Eq.11 noting that the molar \( c_t \) in this expression is dimensionless.

It is useful to first specify \( K_{pt} \) of the reference state corresponding, as discussed in Design of Oligonucleotide Microarray Experiments, to \( K_{pt} \) of the bulk reaction \( p + t = pt \). (17)
The equilibrium condition $\mu_t + \mu_p = \mu_{pt}$ yields $K_{pt} = K_{pt}$ with

\[
K_{pt} = \exp \left\{ -\frac{\Delta G_{pt}^0 + N_A \gamma_{mush}(N - n) + G_{int}^{1:1} - G_{coil}(n) - G_{coil}(N)}{RT} \right\}
\]

where $K_{pt}^0 = \exp(-\Delta G_{pt}^0/RT)$ and $\Delta G_{pt}^0 = \mu_{pt}^0 - \mu_t^0 - \mu_p^0$. $K_{pt} > K_{pt}^0$ because the hybridization results in the formation of a rodlike ds domain whose monomers experience only short-range interactions with each other but also long-range interactions with the monomers of the unhybridized ss tails.

The chemical potentials $\mu_{pt}$ and $\mu_t$ are specified by the free energy per probe site of the surface, $\gamma_{site}$. In the 1:1 regime, when $\Sigma_0 > R_F^2 > r_T^2$, there is no mutual interaction between the probes or between the targets. The molar free energy of probe sites is

\[
\gamma_{site} = \gamma_0 + x \left[ \mu_{pt}^0 + N_A \gamma_{mush}(N - n) + N_A G_{int}^{1:1} + (1 - x) \left[ \mu_p^0 + N_A \gamma_{mush}(n) \right] - TS[x] \right].
\]

Here $\gamma_0$ is the free energy density of the bare surface while $\mu_{pt}^0$ and $\mu_p^0$ denote the chemical potentials of the hybridized and non-hybridized probes in the standard state. As noted before, the standard state of $p$ is an ideal coil with no excluded volume interactions. The two $G_{mush}$ terms allow for the excluded volume and screened electrostatic interactions as well as for the effect of the impenetrable wall. $G_{mush}(N - n)$ accounts for the monomer-monomer interactions of the unhybridized tail of $pt$ while $G_{mush}(n)$ allows for the contribution of the unhybridized probe. $G_{int}^{1:1}$ reflects the electrostatic and excluded volume interactions between the hybridized target and its own probe. The mixing entropy per mole of $p$ and $pt$ sites is $S[x] = -R x \ln x + (1 - x) \ln(1 - x)$.

The equilibrium condition $\mu_{pt} = \mu_t + \mu_p$ can be expressed in terms of the exchange chemical potential of the hybridized probe, $\mu_{pt}^0 = \mu_p - \mu_t = \partial \gamma_{site}/\partial x$, as $\mu_{pt}^0 = \mu_t$. The hybridization isotherm, thus obtained, assumes the familiar Langmuir form

\[
\frac{x_{eq}}{1 - x_{eq}} = c_i K_{pt}^{1:1} = c_i K_{pt}^0 \exp \left[ -\frac{G_{mush}(N - n) + G_{int}^{1:1} - G_{mush}(n) - G_{coil}(N)}{kT} \right]
\]

\[
\simeq c_i K_{pt} \left( \frac{n}{N} \right)^{2/5}.
\]

$K_{pt}^{1:1}$ is smaller than $K_{pt}$ because of the effect of an impenetrable wall giving rise to the $(n/N)^{2/5}$ factor reflecting the reduction in the number of configurations available to the unhybridized tail of $pt$.

In the $\Sigma_0 > R_F^2 > r_T^2$ range the hybridization behavior is independent of $x$. As noted earlier, an $x$ dependence is expected when $R_F^2 < \Sigma_0 > r_T^2$. We first discuss the 1:q regime occurring when $x < x_B$. $\gamma_{site}$ in this range is similar to the one describing the 1:1 regime. The only difference is the replacement of $G_{int}^{1:1}$ by $G_{int}^{1:q}$, thus allowing for the interactions between a hybridized target and $q > 1$ probes. The hybridization isotherm as obtained from $\mu_{pt}^0 = \mu_t$ is

\[
\frac{x_{eq}}{1 - x_{eq}} = c_i K_{pq}^{1:q} = c_i K_{pt}^0 \exp \left[ -\frac{G_{mush}(N - n) + G_{int}^{1:q} - G_{mush}(n) - G_{coil}(N)}{kT} \right]
\]

\[
\simeq c_i K_{pt} \left( \frac{n}{N} \right)^{2/5} \exp \left[ -\frac{n}{N^{4/5}}(q - 1) \right].
\]

As in the 1:1 regime, the hybridization isotherm is of the Langmuir form. The equilibrium constant, $K_{pq}^{1:q}$ is however smaller than $K_{pq}^{1:1}$ because $G_{int}^{1:q}$ is larger than $G_{int}^{1:1}$ by a factor of $q = R_F^2/\Sigma_0 = N^{5/6}a^2/\Sigma_0$.

When $\Sigma \leq R_F^2$ or $x \geq x_B = \Sigma_0/R_F^2 \simeq N^{-6/5}\Sigma_0/a^2$ the hybridized targets begin to crowd each other and form a brush. This crossover occurs at $x_{eq} = x_B$ corresponding to

\[
c_B = \frac{\Sigma_0}{R_F^2 - \Sigma_0 K_{pq}^{1:q}} = \frac{\Sigma_0}{R_F^2 - \Sigma_0 K_{pt} \left( \frac{N}{n} \right)^{2/5}} \exp \left[ -\frac{n}{N^{4/5}}(q - 1) \right].
\]

$\gamma_{site}$ of the brush regime,

\[
\gamma_{site} = \gamma_0 + x[\mu_{pt}^0 + N_A \gamma_{brush}(x) + N_A G_{int}^{1:q}(x)] + (1 - x)[\mu_p^0 + N_A \gamma_{mush}(n)] - TS[x],
\]

is distinctive in two respects. First, $G_{mush}(N - n)$ is replaced by an $x$ dependent free energy of a chain in a brush, $G_{brush}(x)$. Second, the term allowing for the target-probe interactions, $G_{int}^{1:q}(x)$, is also a function of $x$. The
The $N^{1/5}$ term, arising from $G_{\text{coil}}(N)$ is expressed as $N^{2/5}(a^2/\Sigma_0)^{2/3}$ to underline the crossover behavior at $x_B$. By construction, this isotherm is only meaningful when $c_t > c_B$ so that $x > x_B$. It deviates strongly from the Langmuir form because of the $x$ dependence of $G_{\text{brush}}$ and $G_{\text{int}}$.

The complete “long tail” hybridization isotherm for the $r_{2}^{B} < \Sigma_{0} < R_{p}^{B}$ case is obtained from Eq.21 and Eq.24. In this isotherm, as in the interaction free Langmuir isotherm (Eq.1), $x_{eq} \rightarrow 1$ as $c_t$ increases. However, the two scenario differ strongly with respect to the range of $c_t$ involved (Fig.2). The saturation in the long tail case occurs at a much higher $c_t$. When $x_{eq}$ vs $c_t$ curves of the two scenario are compared over a limited $c_t$ range (Fig.2a), the long tail isotherm is superficially similar to a Langmuir isotherm but with apparent saturation at $x_{eq} \ll 1$. A plot of $x_{eq}$ vs log $c_t$ (Fig.2b) is necessary in order to visualize the differences in the saturation behavior.

The $N^{1/5}$ dependence of the sensitivity of the DNA chip is the $c_{50}$ corresponding to the target concentration, $c_t$, needed to obtain at equilibrium $x_{eq} = 1/2$ (Halperin et al., 2004a). The $c_{50}$ also provides a rough estimate for the onset of saturation, as discussed earlier. In the $1:1$ regime, where the hybridization follows a Langmuir isotherm, $c_{50}^{1:1} = 1/K_{pt}^{1:1}$. When $R_{p}^{B} > \Sigma_{0} > r_{2}^{B}$, we can distinguish between two scenarios. So long as $x_B = \Sigma_0/R_{p}^{B} > 1/2$, $x_{eq} = 1/2$ is attained before the onset of the brush and $c_{50}^{B} = 1/K_{pt}^{1:q}$. In the opposite case, $x_B = \Sigma_0/R_{p}^{B} < 1/2$, $x_{eq} = 1/2$ occurs in the brush regime and $c_{50}^{B} = 1/K_{pt}(x_{eq} = 1/2)$. These corresponding experimental guidelines assume a more useful form when considering the logarithm of $c_{50}$. In particular, these relate the range of expected target concentrations $c_t$, as given by $c_{50}^{1:q}$ or $c_{50}^{B}$, to $\Delta G_{pt}^{0}, n, N$ and $\Sigma_0$

$$\ln c_{50}^{1:q} = \frac{\Delta G_{pt}^{0}}{RT} + \frac{2}{5} \ln N + \frac{N^{2/5} a^2}{\Sigma_0} - n^{1/5},$$

$$\ln c_{50}^{B} = \frac{\Delta G_{pt}^{0}}{RT} + \frac{1}{3} \ln \frac{2 \Sigma_0}{n^{6/5} a^2} + [N(1 - 2^{2/3} x_B^{2/3}) + 2n] \left( \frac{a^2}{2 \Sigma_0} \right)^{2/3} - n^{1/5}.$$  

$\Delta G_{pt}^{0}$ can be significantly higher than $c_{50}^{1:q}$,

$$\ln \frac{c_{50}^{B}}{c_{50}^{1:q}} = [N(1 - 2^{2/3} x_B^{2/3}) + 2n] \left( \frac{a^2}{2 \Sigma_0} \right)^{2/3} - N^{2/5} a^2 \Sigma_0 + \frac{1}{3} \ln \frac{2 \Sigma_0}{R_{p}^{B}} \gg 1,$$

since it is dominated by the factor $\exp[N(1 - 2^{2/3} x_B^{2/3})/(a^2/2 \Sigma_0)^{2/3}]$. It is helpful to compare Eq.26 and Eq.27 with the Langmuir isotherm of the “reference” state, Eq.1 where $c_{50}^{B} = 1/K_{pt}$. The guideline obtained, following the same procedure, is

$$\ln c_{50}^{0} = \frac{\Delta G_{pt}^{0}}{RT} + \frac{n}{N^{1/5}} - n^{1/5}.$$  

In this case $c_{50}$ is determined by $n, N$ and $\Delta G_{pt}^{0}/RT$. In marked contrast $c_{50}^{1:q}$ and $c_{50}^{B}$ depends explicitly on $\Sigma_0$. The strong $N$ dependence of $c_{50}^{B}$, as compared to $c_{50}^{1:q}$ and $c_{50}^{0}$, is illustrated in Fig.3. The increase of $c_{50}^{B}$ signals a corresponding loss of sensitivity.

To utilize these guidelines one needs $\Delta G_{pt}^{0}$ as calculated using the nearest neighbor model. However, to highlight the role of $n$ as a design parameter, it is helpful to use the Wetmur approximation (Wetmur, 1991) where average values of the nearest neighbor contributions are utilized. Accordingly, $\Delta G_{pt}^{0}$ of perfectly matched probe-target pair, when the hybridization site is located within the target, is approximated by

$$\Delta G_{pt}^{0} = (n - 1)\Delta H_{nn} + \Delta H_{t} + 2\Delta H_{e}$$ 

where $\Delta H_{nn}, \Delta H_{t}$ and $\Delta H_{e}$ are the average values corresponding to a nearest neighbor pair, an initiation step and a dangling end. Wetmur estimated the nearest neighbor contribution by $\Delta H_{nn} = 8.0 \text{kcal.mol}^{-1}$ and $\Delta S_{nn} = -21.5 \text{cal.mol}^{-1}.K^{-1}$, the initiation term by a temperature independent $\Delta H_{i} = 2.2 \text{kcal.mol}^{-1}$ and the dangling end contribution by $\Delta H_{e} = 8.0 \text{kcal.mol}^{-1}$ and $\Delta S_{e} = -23.5 \text{cal.mol}^{-1}.K^{-1}$. Note that while useful, the Wetmur approximation erroneously predicts identical $\Delta G_{pt}^{0}$ for all $pt$ pairs with $N = n.$
BRUSH EFFECTS–KINETICS OF HYBRIDIZATION

Having obtained the equilibrium constants $K_{pt}^{1:1}$, $K_{pt}^{1:q}$ and $K_{pt}^{B}(x)$ for the hybridization at the surface we are now in a position to consider the corresponding rate constants. To this end we will assume, and later confirm, that the rate is reaction controlled. Again, for simplicity, we set numerical prefactors to unity, $v = a^{3}$ and $l_{p} = a$. It is necessary to recall first the relevant features of the kinetics of oligonucleotide hybridization and of the desorption of polymers out of a brush.

As discussed in Design of Oligonucleotide Microarray Experiments, the reference state of our analysis is a layer of non-interacting probes bound to a passivated surface by long flexible spacers. We assume that the molecular mechanism of hybridization in this case is identical to the bulk one and that the kinetics follow the Langmuir rate
FIG. 3: Plots of \( \log c^B_{50} \) vs \( N \) for the probes utilized by Guo et al. (1994) with \( \Sigma_0 = 2500 \text{Å}^2 \) (—–) and \( \Sigma_0 = 5000 \text{Å}^2 \) (- - -). 

\( T = 30^\circ\text{C} \) and \( n = 15 \). The reference state \( \log c^B_{50} \) is plotted for comparison (···). The circles correspond to the crossover between \( 1 : 1 \) and \( 1 : q \) regimes whereas squares correspond to the crossover between \( 1 : q \) and \( B \) regimes.

law

\[
\frac{dx}{dt} = k_h c_t (1 - x) - k_d x.
\]

In this regime the hybridization and denaturation rate constants, \( k_h \) and \( k_d \), are independent of \( \Sigma_0 \) or \( x \) and approach their bulk values. At equilibrium \( \frac{dx}{dt} = 0 \) leading to \( K_{pt} = k_h/k_d \) as required by detailed balance. In turn, the hybridization mechanism of free oligonucleotides in solution is thought to involve the steps outlined below (Craig et al., 1971; Förschke and Eigen, 1971; Cantor and Schimmel, 1980; Turner, 2000). An approach and alignment of the single stranded oligonucleotides is followed by the hybridization of a single base pair. A stable nucleus, comprising of \( n_c + 1 \) base pairs, is formed by step-wise addition of hybridized pairs. Importantly, a ds sequence of \( n \leq n_c \) is unstable. Once \( n_c + 1 \) is attained the ds domain is rapidly “zipped up”. For oligonucleotides comprising GC base pairs \( n_c \simeq 2 - 3 \) and the hybridization rate constant exhibits the form \( k_h = \tau_h^{-1} \exp[-\Delta G^h_0/RT] \). Here \( \tau_h \) is a molecular time scale characterizing the formation of the last base pair of the nucleus while the activation free energy \( \Delta G^h_0 \) reflects the formation of a ds nucleus of \( n_c \) base pairs plus the activation free energy for adding the next base pair. Importantly, the reaction is not diffusion controlled but involves a number of activation barriers associated with a corrugated free energy profile (Turner, 2000). A rough estimate of \( \Delta G^p_0 \) within the Wetmur approximation (Wetmur, 1991) yields \( \Delta G^p_0 \simeq n_c \Delta G_{nn} + \Delta G_i + 2 \Delta G_e \) indicating that \( \Delta G^p_0 \) depends on \( n_c \) rather than \( n \). This last point rationalizes a phenomenological result we will utilize later, namely \( k_h \) in high ionic strength solutions is

\[
k_h \simeq 10^6 M^{-1} s^{-1}
\]

(31)
to within one order of magnitude and with a weak \( T \) dependence (Turner, 2000). This, together with the detailed balance requirement \( K_{pt} = k_h/k_d \) yields

\[
k_d \simeq 10^6 \exp[\Delta G_{pt}^0/RT] s^{-1}.
\]

(32)

In terms of the Wetmur approximation \( k_d \) is expressed as \( k_d \simeq \tau_h^{-1} \exp[(n - n_c)\Delta G_{nn}/RT] \). The activation barrier for denaturation involves thus the break up of \( n - n_c \) base pairs so as to form an unstable ds domain. Importantly, for \( 15 \leq n \leq 25 \), the denaturation life time at \( 37^\circ\text{C} \) is measured in years.

At this point it is of interest to comment on a result, obtained from computer simulations, concerning the kinetics of desorption out of a brush (Wittmer et al., 1994). It concerns a planar brush formed from flexible and neutral chains whose terminal monomer experience a short range attraction to the wall. The attraction was modeled as a well of
width $a$, a monomer size, and depth $G_{\text{well}}$. In this system the expulsion rate constant is

$$k_{\text{out}} = \tau^{-1}\langle \Sigma \rangle \exp[-G_{\text{well}}/RT]$$

(33)

where $\tau(\Sigma)$ is the time required by the head group to diffuse across a distance $\Sigma^{1/2}$, corresponding to the inner most blob of the brush. Importantly, $k_{\text{out}}$ while $\Sigma$ dependent was found to be independent of $N$. Once the surface bond is broken, the expulsion of the chain out of the brush is driven by repulsive monomer-monomer interactions with neighboring chains. This last stage is a fast process and thus not rate controlling. The system studied by Wittmer et al. differs from ours in two respects. First, in this study the attractive potential is laterally invarient i.e., the surface is uniformly attractive. As a result, the reaction coordinate is the distance between the terminal end group and the surface. In our case the attractive potential is localized at the immediate vicinity of the probe and the early steps of denaturation involve lateral separation of the two strands. Consequently the reaction coordinate at the vicinity of the surface is no longer $z$. Second, in the work of Wittmer et al., the barrier to adsorption is due to the brush. There is no barrier in the mushroom regime where the reaction is diffusion controlled. This is also the case in the brush regime when the terminal group resides within a distance $\Sigma^{1/2}$ from the surface. However, as noted earlier the hybridization reaction in the bulk is not diffusion controlled. Accordingly, one should consider the possibility that the rate of hybridization at the surface is similarly not controlled by diffusion. In such a case the denaturation rate constant, corresponding to $k_{\text{out}}$, will be independent of both $N$ and $\Sigma$.

In the following we will assume, and later confirm, that the rate of hybridization at the surface is reaction controlled rather than diffusion controlled. In quantitative terms, the assumption of reaction control involves two ingredients. First, the rate equation may be written as

$$\frac{dx}{dt} = k_{h}c_{t}(z = 0)(1 - x) - k_{d}x$$

(34)

where $c_{t}(z = 0)$ is the local concentration of target hybridization sites at the surface while $k_{h}$ and $k_{d}$ stand for the rate constants as observed in the solution. In microscopic terms this implies that the hybridization and denaturation reactions at the surface are respectively monomolecular and bimolecular and that the encounter probability between a probe and a target is proportional to $c_{t}(z = 0)$. Importantly it also implies that the free energy surfaces of the hybridization reaction in the bulk and at the surface are identical. This last point is reasonable because this free energy surface reflects local reorganization of hydrogen bonds and stacking interactions (Turner, 2000). This assumption also implies that the lateral diffusion is fast enough so as to prevent inplane variation of $c_{t}(z = 0)$. The second ingredient is the assumption that, for any $x$, $c_{t}(z = 0)$ is equal to $c_{t}^{*}(x)$, the equilibrium concentration of unhybridized terminal groups at the surface. In other words, the diffusion of chains is sufficiently fast in comparison to the hybridization reaction to ensure that a Boltzmann distribution is maintained. This condition is especially stringent in the brush regime, where in- and out diffusion must overcome a potential barrier due to interactions with the previously tethered chains. The equilibrium condition requires that $c_{t}^{*}/c_{t} = \exp(-\Delta\mu/RT)$ where $\Delta\mu(x)$ is the difference between the chemical potential of a fully inserted chain and a free one. Accordingly, for each of the three regimes

$$\frac{c_{t}^{*}}{c_{t}} = \frac{K_{pt}^{i}}{K_{pt}}$$

(35)

Note that within our treatment numerical prefactors are omitted and there is no distinction between the chemical potential and the free energy per chain. Altogether, the corresponding rate constants for the three regimes, $i = 1 : 1, 1 : q$ and $B$ are

$$k_{i}^{h} = k_{h}K_{pt}^{i} \quad \text{and} \quad k_{i}^{d} = k_{d}$$

(36)

leading to

$$k_{h}^{B}(x) \simeq k_{h}\left( \frac{n^{6/5}a^{2}x}{\Sigma_{0}} \right)^{1/3} \exp \left[ -\frac{n}{N^{4/5}} \left[ N(x^{2/3} - x_{B}^{2/3}) + nx^{-1/3} \right] \right] \left( \frac{a^{2}}{\Sigma_{0}} \right)^{2/3}.$$  

(37)

$$k_{h}^{1/q} \simeq k_{h}\left( \frac{n}{N} \right)^{2/5} \exp \left[ -\frac{n}{N^{4/5}}(q - 1) \right].$$

(38)

$$k_{h}^{1:1} \simeq k_{h}\left( \frac{n}{N} \right)^{2/5}.$$  

(39)

The results above where obtained assuming that the hybridization rate is controlled by the reaction rather than by the diffusion towards the surface. To check the consistency of this approach we consider the corresponding Damköhler
FIG. 4: The hybridization kinetics, as described by a plot of $x$ vs the time $t$ in hours, for the probe target pairs of Guo et al. (1994): $n = 15$, $T = 30^\circ C$, $c_t = 1 \text{ nM}$ and $\Sigma_0 = 5000 \text{ Å}^2$. The $N = 157$ (—–) and $N = 347$ ( - - - ) curves are compared to the reference state case with $N = 157$ ( - - - ).

number (Blanch and Clark, 1996) $Da = J_{\text{reac}}/J_{\text{dif}}$. Here $J_{\text{reac}}$ and $J_{\text{dif}}$ are the maximal fluxes associated with the reaction and the inbound diffusion, assuming reaction control. Reaction control implies $Da \ll 1$. $J_{\text{reac}} = k_h c_t^*/\Sigma_0$ is an upper bound on the reaction flux. The inbound flux of chain through the brush is $J_{\text{dif}} = c_t^* v_{\text{barrier}}$ where $v_{\text{barrier}}$ is the diffusion velocity of a single chain at the vicinity of the surface where the brush potential is essentially flat. Recent experimental results and a unified picture of the theoretical models are presented by Titmuss et al. (2004).

Altogether

$$Da = \frac{k_h}{\Sigma_0 v_{\text{barrier}}}$$

(40)

where $v_{\text{barrier}} = \alpha kT/\eta N a^2$. Here $\eta$ is the solvent viscosity and $\alpha$ is a polymer specific numerical constant. $\alpha$ of ssDNA has not yet been determined but for flexible synthetic polymer $\alpha \simeq 0.1$. For water at $25^\circ C \eta = 0.89 \times 10^{-3} \text{ N.m}^{-2} \text{.s}$. The Damköhler number at $25^\circ C$, when both fluxes are expressed in units of chains.$m^{-2}.s^{-1}$ is

$$Da = 0.13 \frac{N}{\Sigma_0}$$

(41)

where we assumed $\alpha = 0.1$, $k_h = 10^6 M^{-1}.s^{-1}$, $a = 6 \text{ Å}$ and expressed $\Sigma_0$ in $\text{Å}^2$. For $100 \leq N \leq 600$ and $T = 25^\circ C$, the Damköhler number varies in the range $9 \times 10^{-3} \leq Da \leq 5 \times 10^{-2}$ when $\Sigma_0 = 1500 \text{Å}^2$ and $2.6 \times 10^{-2} \leq Da \leq 0.16$ when $\Sigma_0 = 500 \text{Å}^2$. The variation of water viscosity with temperature affects those ranges by at most a factor 2 for $0^\circ C \leq T \leq 70^\circ C$. Accordingly, the assumption of reaction control of the hybridization rate is justified for typical values of $N$ and $\Sigma_0$. It will though fail eventually for high $N$ values. One should note that the issue of reaction vs diffusion also arise when the hybridization chamber is agitated and we will not discuss it further.

As required the rate constants Eq. 37-39 obey detailed balance and exhibit the proper crossover behavior. In particular, $k_h^0/k_d = K_{\text{hit}}^0$ as well as $k_h^B(x_B) = k_h^{1-q}$. The $x$ dependence of $k_h^B$ slows down the adsorption rate (Fig.4). $k_h^B(x_{co}) = k_h/e$ is a possible measure for the onset of significant slow down. In the limit of $N \gg 2n$ the $x^{-1/3}$ term is negligible and the onset occurs roughly at

$$x_{co} = \left[ \frac{1}{N} \left( \frac{\Sigma_0}{a^2} \right)^{2/3} + x_{B}^{2/3} \right]^{3/2} \simeq x_B.$$  

(42)

It thus affects the whole brush regime. The slower kinetics in the brush regime can affect the attained hybridization
even after long hybridization periods (Fig. 5). This is of practical importance because samples of identical $c_t$ but different $N$ will vary in their signal intensity.

**DISCUSSION**

The relative size of the targets and probes is an important characteristic of oligonucleotides microarrays. When the two are of equal size, $N = n$, the onset of interaction between the probes is roughly set by the span of the probes as determined by $n$. In biology experiments the targets are much larger, $N \gg n$, and the onset of interactions is controlled by $N$. The progress of hybridization can give rise to crowding of the non-hybridized tails when $R_P^2 > \Sigma_0$.

The polyelectrolyte brush thus formed affects the hybridization isotherm and the rate equations. In particular, it lowers both the hybridization rate and the attainable hybridization for a given concentration of targets. It is important to allow for this effect in the design of DNA microarrays, in the formulating of the protocols of sample preparation and hybridization as well as in the analysis of the results. With regard to design of DNA chips the brush effect is important in choosing the desired density of oligonucleotide probes, or equivalently $\Sigma_0$. The brush effect will lower the fraction of probes that actually hybridize. As a result, the benefits of increasing the surface density of oligonucleotide probes diminish when the intended targets are long. When $\Sigma_0$ is set, these considerations suggest a criteria for tuning the length of the targets, $N$, as controlled by the choice of the PCR primers or of the fragmentation procedure. In particular, it is beneficial to shorten $N$ so as to avoid crowding. When brush effects do occur the analysis of the results should allow for the ensuing deviations from the Langmuir behavior. This is an important point for the implementation of model based algorithms.

Physical chemistry type experiments, that aim to investigate the function of DNA microarrays, tend to focus on the symmetric case, of $N = n$. Our discussion highlights the merit of studying the kinetics and the equilibrium behavior in the asymmetric case, $N \gg n$. In this case it is of interest to correlate the hybridization behavior with measurements of the brush thickness.

Our analysis focused on the case of ssDNA targets so as to avoid complications due to the secondary structure of RNA molecules. The importance of the secondary structure of RNA targets, as used in gene expression experiments, is yet to be established because the effect of labelling by biotin is not well understood. The effect of the fragmentation on the kinetics of hybridization suggests however that a crowding effect of some sort is indeed involved.
APPENDIX A: THE VIRIAL COEFFICIENT AND THE CASE OF A BRUSH OF RODS

Consider first the second virial coefficient

\[ v = \frac{1}{2} \int_0^\infty \left[ 1 - \exp\left( -\frac{U(r)}{kT} \right) \right] 4\pi r^2 dr \]  \hspace{1cm} (43)

for spherical monomers of radius \( a \) when their interactions are purely repulsive. In particular, the interaction potential, \( U(r) \), comprises a hard core repulsion together with a screened electrostatic repulsion, that is

\[ U = \begin{cases} \infty & \text{for } r < a, \\ \frac{kT l_B \exp\left[ -\frac{(r - a)}{r_D} \right]}{r} \frac{1}{1 + a/r_D} & \text{for } r > a. \end{cases} \]  \hspace{1cm} (44)

Here \( r_D \) is the Debye screening length and \( l_B \) is the Bjerrum length (Fowler and Gugenheim, 1960). The hard core contribution to \( v \) is \( 2\pi a^3/3 \). The electrostatic contribution, assuming that \( U/kT \ll 1 \), is \( 2\pi l_B r_D^2 \) and altogether

\[ v = \frac{2\pi}{3} a^3 + 2\pi l_B r_D^2. \]  \hspace{1cm} (45)

If one supplements the electrostatic repulsion \( U \) by a weak van der Waals attraction the first term assumes the form \( 2\pi a^3(1 - \theta/T)/3 \) where \( \theta \) is the theta temperature (Rubinstein and Colby, 2003) thus leading to Eq.10. For \( 0.1M \) of \( NaCl \) salt, \( r_D = 10\AA \) and assuming \( a = 6\AA \) we find that the electrostatic term dominates. When the salt concentration is \( 1M \) the screening length diminishes to \( r_D = 3\AA \) and the two terms are comparable.

In the case of probes and targets of equal length, \( n = N \), the probe layer consists of a mixture of single stranded probes and hybridized, double stranded ones. The associated interaction free energy for this case can be obtained (Halperin et al., 2004a) upon assuming, following Korolev et al. (1998), that both adopt rod-like configurations of equal length \( L = nb \) where \( b \simeq 3.4\AA \) is the contribution of a base (base pair) to the length of the rod. The hybridized probes are rod-like because a dsDNA is rigid on the length scales of a typical probe \( (10 < n \leq 30) \). Viewing the unhybridized probes as rigid rods is an approximation justified, for the short probes, by two related observations. One is the tendency of ssDNA to form rigid domains of single stranded helices due to stacking interactions (Cantor and Schimmel, 1980; Turner, 2000; Buhot and Halperin, 2004). The second is that the persistence length attributed to ssDNA is comparable to the length of the probes. It is important however to stress that the configurations of ssDNA are not yet fully characterized. As noted in Design of Oligonucleotide Microarray Experiments, the reported values of the persistence length of ssDNA vary over a wide range \( 7.5\AA \leq l_p \leq 35\AA \). Similarly, the thermodynamic parameters of the stacking interactions are not fully established. With these reservations in mind, this picture provides a convenient approximation because it allows us to assign to the probe layer a unique thickness, independent of \( n \).

The interaction free energy density within the probe layer is

\[ \gamma_{el} = \frac{2\pi l_B r_D^2 n^2 (1 + x)^2}{\Sigma_0 L}. \]  \hspace{1cm} (46)

Accordingly, the overall free energy per probe site

\[ \gamma_{site} = \gamma_0 + x\mu_{pt}^0 + (1 - x)\mu_p^0 + \Sigma_0 \gamma_{el}(x) + RT[x \ln x + (1 - x) \ln(1 - x)] \]  \hspace{1cm} (47)

and the equilibrium condition \( \mu_t = \mu_{pt}^c = \partial \gamma_{site} / \partial x \) yields

\[ \frac{x_{eq}}{1 - x_{eq}} = c_l K_{pt} \exp\left[ -\Gamma(1 + x_{eq}) \right] \]  \hspace{1cm} (48)

with \( \Gamma = 4\pi n^2 l_B r_D^2 / \Sigma_0 L \), as obtained earlier using the box approximation for the solution of the Poisson-Boltzmann equation (Halperin et al., 2004a) with a different prefactor. The isotherm obtained above differs from the “brush isotherm” because the chain elasticity does not play a role and the layer thickness does not exhibit an \( x \) dependence.

APPENDIX B: EFFECT OF CHAIN SELF-AVOIDANCE ON THE HYBRIDIZATION CONSTANTS

The Flory approximation as used in the text overestimates both the elastic and interaction free energies. Another delicate point concerns the entropy of the free ends. At the same time, the Flory approximation is known to be robust.
and its performance for the brush has been studied showing relatively mild deviation from the exact results obtained by SCF theory (Milner, 1991). With these points in mind it is of interest to confirm the results obtained utilizing the Alexander-Flory approximation by a more rigorous approach. In the following we present exact results concerning $K^{1:1}$. In particular, the alternative derivation allows for the chain self-avoidance while ignoring the small correction due to interactions between the hybridized $ds$ domain and unhybridized tail of the target. To this end we utilize the partition function of a self-avoiding chain (Duplantier, 1989; Eisenrigler et al., 1982). The partition function $Z_{\text{coil}}(N)$ of a free self-avoiding chain of $N$ monomers is

$$Z_{\text{coil}}(N) = z^N N^{\gamma-1}$$  \tag{49}$$

where $z$ is model-dependent effective partition function of a monomer, and $\gamma$ is a universal configurational exponent. For a self-avoiding chain with a terminal monomer anchored to an impenetrable planar surface, a “mushroom”, the partition function is

$$Z_{\text{mush}}(N) = z^N N^{\gamma_1-1}$$  \tag{50}$$

where $\gamma_1$ is a different universal configurational exponent.

When a probe and a target hybridize, the $ds$ domain can be envisioned as a rigid rod with a partition function

$$Z_{\text{rod}}(n) = z_{\text{rod}}^n = z_0^n \exp[-\Delta G_{pt}^0(n)/RT]$$  \tag{51}$$

Here, $z_{\text{rod}}$ is the partition function of a pair of hybridized monomers, $z_0$ is partition function of a single monomer in an ideal Gaussian coil, $n$ is number of pairs in the $ds$ domain, and $\Delta G_{pt}^0(n)$ is the free energy difference between the rigid $ds$ and ideal coil $ss$ domains. The free energy $G$ is related to partition function $Z$ by $G = -RT \ln(Z)$.

The hybridization constant $K_{pt}$ in a solution of targets and probes whose respective lengths are $N$ and $n \ll N$ is

$$K_{pt} = \exp\{-[G_{\text{rod}}(n) + G_{\text{coil}}(N-n) - G_{\text{coil}}(N) - G_{\text{coil}}(n)]/RT\}$$  \tag{52}$$

Using Eq.\ref{eq:49}, Eq.\ref{eq:50} and Eq.\ref{eq:51} we obtain

$$K_{pt} \approx K_{pt}^0 n^{1-\gamma} \left(\frac{z_0}{z}\right)^{2n}$$  \tag{53}$$

where $K_{pt}^0 = \exp[-\Delta G_{pt}^0/RT]$ as introduced earlier.

For the hybridization at a surface in the $1:1$ regime

$$K_{pt}^{1:1} = \exp\{-[G_{\text{rod}}(n) + G_{\text{mush}}(N-n) - G_{\text{coil}}(N) - G_{\text{mush}}(n) - \delta S_{\text{rod}}]/RT\}$$  \tag{54}$$

Here, $\delta S_{\text{rod}} \equiv \ln(\beta)$ is the reduction in the rod entropy due to its attachment to the surface. The specific value of $\beta$ of the order of unity depends on the length and flexibility of the spacer. In the simplest case of a short flexible spacer, the surface eliminates half of space available to a free rod in the solution, thus yielding $\beta = 1/2$. Eq.\ref{eq:49}, Eq.\ref{eq:50} and Eq.\ref{eq:51} lead to

$$K_{pt}^{1:1} = \beta \frac{Z_{\text{rod}}(n) Z_{\text{mush}}(N-n)}{Z_{\text{mush}}(n) Z_{\text{coil}}(N)} = \beta \left(\frac{N-n}{n}\right)^{\gamma_1-1} N^{1-\gamma} \left(\frac{z_0}{z}\right)^{2n} \exp[-\Delta G_0(n)/RT]$$  \tag{55}$$

The ratio of hybridization constants at the surface and in solution, as determined from Eq.\ref{eq:54} and Eq.\ref{eq:55} is

$$\frac{K_{pt}^{1:1}}{K_{pt}} = \beta \left(\frac{n}{N}\right)^{\gamma-\gamma_1} \quad N \gg n$$  \tag{56}$$

The values of $\gamma \approx 1.167$ and $\gamma_1 \approx 0.695$ were obtained using field theoretical methods and numerical calculations (Duplantier, 1989; Eisenrigler et al., 1982). Therefore, $\gamma - \gamma_1 \approx 0.47$ is in close agreement with $K_{pt}^{1:1}/K_{pt} = (n/N)^{2/5}$, Eq.\ref{eq:20}.
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REFERENCES

Affymetrix. 2004. GeneChip Expression Analysis. Technical Manual. WebSite: http://www.affymetrix.com/support/technical/manuals.affx

Alexander, S. 1977. Adsorption of chain molecules with a polar head - a scaling description. J. Phys. (Paris) 38:983-987.

Birshtein, T. M., Yu. V. Liatskaya, and E. B. Zhulina. 1990. Theory of supermolecular structure of polydisperse block copolymers: 1. planar layers of grafted chains. Polymer 31:2185-2196.

Birshtein, T. M., and E. B. Zhulina. 1984. Conformations of star-branched macromolecules. Polymer, 25:1453-1461.

Bhanot, G., Y. Louzoun, J. Zhu, and C. DeLisi. 2003. The importance of thermodynamic equilibrium for high throughput gene expression arrays. Biophys. J. 84:124-135.

Blanch, H. W., and D. S. Clark. 1996. Biochemical Engineering. Marcel Dekker, New York.

Borisov, O. V., T. M. Birshtein, and E. B. Zhulina. 1991. Collapse of grafted polyelectrolyte layer. J. Phys. II. 1:521-526.

Buhot, A., and A. Halperin. 2004. Effects of stacking on the configurations and elasticity of single-stranded nucleic acids. Phys. Rev. E 70:020902(R).

Cantor, C. R., and P. R. Schimmel. 1980. Biophysical Chemistry. WH Freeman, New York.

Chan, V., D. J. Graves, and S. McKenzie. 1995. The biophysics of DNA hybridization with immobilized oligonucleotide probes. Biophys. J. 69:2243-2255.

Craig, M. E., D. M. Crothers, and P. Doty. 1971. Relaxation kinetics of dimer formation by self complementary oligonucleotides. J. Mol. Biol. 62:383-392.

Dai, H., M. Meyer, S. Stepaniants, M. Ziman, and R. Soughton. 2002. Use of hybridization kinetics for differentiating specific from non-specific binding to oligonucleotide microarrays. Nucleic Acids Res. 30:e86.

De Gennes, P. G. 1979. Scaling Concepts in Polymer Physics. Cornell University Press, Ithaca, New York, USA.

DiMarzio, E. A. 1965. Proper Accounting of Conformations of a Polymer Near a Surface. J. Chem. Phys. 42:2101-2106.

Duplantier, B. 1989. Statistical Mechanics of Polymer Networks of Any Topology. J. Stat. Phys. 54:581-680.

Eisenriegler, E., K. Kremer, and K. Binder 1982. Adsorption of Polymer Chains at Surfaces: Scaling and Monte Carlo Analyses. J. Chem. Phys. 77:6296-6320.

Evans, D. F., and H. Wennemerström. 1994. The Colloid Domain. VHC, New York.

Forman, J. E., I. D. Walton, D. Stern, R. P. Rava, and M. O. Trulson. 1998. Thermodynamics of duplex formation and mismatch discrimination on photolithographically synthesized oligonucleotide arrays. ACS Symp. Ser. 682:206-228.

Fowler, R. and E. A. Gugenheim. 1960. Statistical Thermodynamics. Cambridge, UK.

Georgiadis, R., K. P. Peterlinz, and A. W. Peterson. 2000. Quantitative Measurements and Modeling of Kinetics in Nucleic Acid Monolayer Films Using SPR Spectroscopy. J. Am. Chem. Soc. 122:3166-3173.

Graves, D. J. 1999. Powerful tools for genetic analysis come of age. Trends Biotechnol. 17:127-134.

Guo, Z., R. A. Guilfoyle, A. J. Thiel, R. Wang, and L. M. Smith. 1994. Direct Fluorescence Analysis of Genetic Polymorphism by Hybridization with Oligonucleotide Arrays on Glass Supports. Nucleic Acids Res. 22:5456-5465.

Halperin, A., M. Tirrell, T. P. Lodge. 1992. Tethered Chains in Polymer Microstructures. Adv. Polym. Sci. 100:31-71.

Halperin, A., A. Buhot, and E. B. Zhulina. 2004a. Sensitivity, specificity and the hybridization isotherms of DNA chips. Biophys J. 86:718-730.

Halperin A., A. Buhot, and E. B. Zhulina. 2004b. Hybridization Isotherms of DNA Chips and the Quantification of Mutation Studies. Clin. Chem. 50:2254-2262.

Hekstra, D., A. R. Taussig, M. Magnusco, and F. Naef. 2003. Absolute mRNA concentrations from sequence-specific calibration of oligonucleotide arrays. Nucleic Acids Res. 31:1962-1968.

Held, G. A., G. Grinstein, and Y. Tu. 2003. Modeling of DNA microarray data by using physical properties of hybridization. Proc. Natl. Acad. Sci. USA 100:7575-7580.

Heller, M. J. 2002. DNA microarray technology: devices, systems and applications. Annu. Rev. Biomed. End 4:129-153.
HyTeq™ version 1.0, Nicolas Peyret and John SantaLucia Jr. Wayne State University. http://ozone2.chem.wayne.edu/Hyther/hytherm1main.html

Kepler, T. B., L. Crosby, and K. T. Morgan. 2002. Normalization and analysis of DNA microarray data by self consistency and local regression. Genome Biol. 3:0037.1-0037.12.

Korolev, N., A. P. Lyubartsev, and L. Nordenskiöld. 1998. Application of Polyelectrolyte Theories for Analysis of DNA Melting in the Presence of Na⁺ and Mg²⁺ Ions. Biophys. J. 75:3041-3056.

Livshits, M. A., and A. D. Mirzabekov. 1996. Theoretical analysis of the kinetics of DNA hybridization with gel-immobilized oligonucleotides. Biophys. J. 71:2793-2801.

Lockhart, D. J., and E. A. Winzeler. 2000. Genomics, gene expression and DNA arrays. Nature 405:827-836.

Mills, J. B., E. Vacano, and P. J. Hagerman. 1999. Flexibility of Single-stranded DNA: Use of Gapped Duplex Helices to Determine the Persistence Lengths of Poly(dT) and Poly(dA). J. Mol. Biol. 285:245-257.

Milner, S. T. 1991. Polymer brushes. Science 251:905-914.

Moore, W. J. 1972. Physical Chemistry. Longman, London, UK.

Naef, F., M. Magnasco. 2003. Solving the riddle of the bright mismatches: Labeling and effective binding in oligonucleotide arrays. Phys. Rev. E 68:011906.

Nelson, B. P., T. E. Grimsrud, M. R. Liles, R. M. Goodman, and R. M. Corn. 2001. Surface Plasmon Resonance Imaging Measurements of DNA and RNA Hybridization Adsorption onto DNA Microarrays. Anal. Chem. 73:1-7.

Okahata, Y., M. Kawase, K. Niikura, F. Otake, H. Furusawa, and Y. Ebara. 1998. Kinetic Measurements of DNA Hybridization on an Oligonucleotide-Immobilized 27-MHz Quartz Crystal Microbalance. Anal. Chem. 70:1288-1296.

Peterson, A. W., L. K. Wolf, and R. M. Georgiadis. 2002. Hybridization of Mismatched or Partially Mismatched DNA at Surfaces. J. Am. Chem. Soc. 124:14601-14607.

Peyret, N., P. A. Seneviratne, H. T. Allawi, and J. SantaLucia. 1999. Nearest-neighbor thermodynamics and NMR of DNA sequences with internal A:A, C:C, G:G, and T:T mismatches. Biochemistry 38:3468-3477.

Pincus, P. 1991. Colloid stabilization with grafted polyelectrolytes. Macromolecules 24:2912-2919.

Pirrung, M. C. 2002. How to make a DNA chip? Angew. Chem. Int. Ed. 41:1277-1289.

Pörschke, D., and M. Eigen. 1971. Co-operative non-enzymatic base recognition III. Kinetics of the helix–coil transition of the oligoribouridylic-oligoriboadenylic acid system and of oligoriboadenylic acid alone at acidic pH. J. Mol. Biol. 62:361-364.

Prix, L., P. Uciechowski, B. Böckmann, M. Giesen, and A. J. Schuetz. 2002. Diagnostic Biochip Array for Fast and Sensitive Detection of K-ras Mutations in Stool. Clin. Chem. 48:428-435.

Rosenow, C., R. M. Saxena, M. Durst, and T. R. Gingeras. 2001. Prokaryotic RNA preparation methods useful for high density array analysis: comparison of two approaches. Nucleic Acids Res. 29:e112.

Rubinstein, M., and R. H. Colby. 2003. Polymer Physics. Oxford University Press, Oxford.

Rühe, J., M. Ballauf, M. Biesalski, P. Dziezok, F. Grohn, D. Johannsmann, N. Houbenov, N. Hugenberg, R. Kouradi, S. Minko, M. Motornov, R. R. Netz, M. Schmidt, C. Siedel, M. Stamm, T. Stephan, D. Usov, and H. N. Zhang. 2004. Polyelectrolyte Brushes. Adv. Polym. Sci. 165:77-150.

SantaLucia, J. 1998. A unified view of polymer, dumbbell, and oligonucleotide DNA nearest-neighbor thermodynamics. Proc. Natl. Acad. Sci. USA 95:1460-1465.

SantaLucia, J., and D. Hicks. 2004. The Thermodynamics of DNA Structural Motifs. Annu. Rev. Biophys. Biomol. Struct. 33:415-450.

Smith, S. B., Y. J. Cui, and C. Bustamante. 1996. Overstretching B-DNA: The elastic response of individual double-stranded and single-stranded molecules. Science 271:795-799.

Southern, E., K. Mir, and M. Shcheuinov. 1999. Molecular interactions on microarrays. Nat. Genet. 21:5-9.

Steel, A. B., T. M. Herne, and M. J. Tarlov. 1998. Electrochemical Quantitation of DNA Immobilized on Gold. Anal. Chem. 70:4670-4677.

Strick, T. R., M.-N. Dessinges, G. Charvin, N. H. Dekker, J.-F. Allemand, D. Bensimon, and V. Croquette. 2003. Stretching of macromolecules and proteins. Rep. Prog. Phys. 66:1-45.

Su, H.-J., S. Surrey, S. E. McKenzie, P. Fortina, and D. J. Graves. 2002. Electrophoresis 23:1551-1557.

Titmuss, S., W. H. Briscoe, I. E. Dunlop, G. Sakellariou, N. Hadjichristidis, and J. Klein. 2004. Effect of end-group sticking energy on the properties of polymer brushes: Comparing experimental evidence and theory. J. Chem. Phys. 121:11408-19.

Turner, D. H. 2000. Chap.8 Conformational Changes. in Bloomfield, V. A., D. Crothers, and I. Tinoco Jr. Nucleic Acids: structures, properties and functions. University Science Books, Sausalito, USA.

Vainrub, A., and M. B. Pettitt. 2002. Coulomb blockage of hybridization in two-dimensional DNA arrays. Phys. Rev. E 66:041905.

Wang, J. 2000. From DNA biosensors to gene chips. Nucleic Acids Res. 28:3011-3016.

Wetmun, J. G. 1991. DNA Probes: Applications of the Principles of Nucleic Acid Hybridization. Crit. Rev. Biochem. Mol. Bio. 26:227-259.
Wittmer, J., A. Johner, J. F. Joanny, and K. Binder. 1994. Chain desorption from semidilute polymer brush: A Monte Carlo simulation. J. Chem. Phys. 101:4379-4390.

Zhang, L., M. F. Miles, K. D. Aldape. 2003. A model of molecular interactions on short oligonucleotide microarrays. Nature Biotechnol. 21:818-821.
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