Evaluation of the impact of EMBRACE II protocol in Spanish centers, with a large cohort of patients using a ranking index

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Abstract

Purpose: The aim of this paper was to assess development of high-dose-rate (HDR) cervix brachytherapy (BT) implants in three Spanish institutions before and after introduction of EMBRACE II protocol.

Material and methods: 392 patients from three different institutions, treated between 2009 and 2019 were analyzed. D90 of high-risk clinical target volume (HR-CTV) and D2cc of organs at risk (OARs) of all patients were collected. Statistical distribution was analyzed for two different periods of time: before and after EMBRACE II publication. Index I was applied based on collected dosimetric quantities (D90 and D2cc) to enhance equilibrium between HR-CTV coverage and doses to OARs. Variation in dosimetry and index depending on CTV and technique used (IC vs. IC/IT) were also evaluated.

Results: Adaptation of institutions to EMBRACE II protocol resulted in a statistically significant increase of D90 HR-CTV (Institution 1; \(p < 0.00001\)) or decrease of D2cc OARs (Institution 2; \(p < 0.04\)). Increase in the use of interstitial component showed higher coverage of HR-CTV for Institution 3 (\(p = 0.03\)), and lower doses to OARs for the same coverage of HR-CTV at Institution 2 (\(p\)-OARs < 0.03). Even though index I was only significantly different between periods for Institution 1 (\(p < 0.0000001\)), it was able to show a reduction of dose variability related to higher expertise and higher interstitial component.

Conclusions: Depending on local protocol before EMBRACE II, the adaptation through increasing interstitial component and physician and physicist training, resulted in a significant increase of HR-CTV doses or reduction of OARs doses. Index I was able to describe an evolution of equilibrium between CTV coverage and OARs’ sparing.

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Purpose

High-dose-rate (HDR) or pulsed-dose-rate (PDR) brachytherapy (BT) have demonstrated an essential role in the curative management of many pathologies, including cervical cancer. Excellent control rates of locally advanced cervical cancer (LACC) have been reported with external beam radiotherapy (EBRT) and concurrent chemotherapy, followed by BT [1, 2].

Technological evolution of EBRT and development of new techniques, such as intensity-modulated radiotherapy (IMRT), volumetric arc therapy (VMAT), or stereotactic body radiotherapy (SBRT) have opened a new range of possible treatments for cervical cancer [3, 4]. However, it has been reported that BT produces high-dose distributions in the target, with higher dose gradients delivered and better sparing of critical organs than EBRT [5, 6]. The Society of Gynecologic Oncology (SGO), the Groupe Europeen de Curiethérapie-European Society of Therapeutic Radiation and Oncology (GEC-ESTRO), and the American Brachytherapy Society (ABS) in their recent recommendations state that the avoidance of BT for cervical cancer has been related to negative consequences affecting survival, and SBRT should not be a substitute for BT in patients undergoing primary curative intent radiation therapy for cervical cancer [5, 7].

Previously, with 2D BT treatment planning, protocols for cervix BT were based on dose points, such as points A or ICRU (International Commission on Radiation Units and Measurements) points [8-10]. Following introduction of computed axial tomography (CT), the access to specific anatomy of patients turn out to be possible, and with
dose-volume histograms (DVH) information, it became available for target volumes and organs at risk (OARs). However, protocols and tolerances were still based on dose points. In 2005-2006, GEC-ESTRO published recommendations for cervix cancer BT, in which T2-weighted magnetic resonance imaging (MRI) was the recommended image modality due to its superior soft tissue contrast, which allowed identification of tumor response during treatment [11, 12]. These guidelines, later collected and supported by the ICRU Report No. 89 [13], introduced and defined a delineation procedure for gross tumor volume (GTV), high-risk clinical target volume (HR-CTV), intermediate-risk clinical target volume (IR-CTV), and OARs, focusing on dose prescriptions and tolerances of 90% and 2 cm³ of these volumes, respectively. Recommendations on dosimetric information, which should be reported included also: reference air-kerma rate (RAKR) of the source, dose to recto-vaginal point and points A, D90 (dose absorbed by 98% of the volume), D2cc, and D50 of HR-CTV, and D3cc, D2cc of the bladder, rectum, sigmoid, and bowel (main OARs).

In 2008, GYN GEC-ESTRO workgroup started EMBRACE (IntErnational Study on MRI-based BRAchy-therapy in Cervical Cancer), with a goal of assessing and validating MRI-guided BT. In this first study, dosimetric quantities introduced previously by GEC-ESTRO and later supported by ICRU (e.g., D90, D2cc) were used, and their recommended values were based on historical and clinical experiences of participating institutions [14]. In 2011, a retrospective project (RetroEMBRACE) began with the aim of analyzing previously treated patients to beginning of EMBRACE [15]. With clinical data obtained from both the studies, the objectives of EMBRACE II study were established [16]. In this last protocol [17], the tolerance, objective, and mandatory values of different dosimetric parameters of each of relevant structures were reported, based on clinical evidence [18].

Recently, De Leeuw et al. [19] presented a report concerning a Dutch national quality assurance program for state-of-the-art curative radiotherapy for patients with LACC. This project was useful to show the need for training concerning the adaptation to the new EMBRACE II treatment protocol. EMBRACE II protocol introduced new tolerance and objective doses for target and OARs volumes. The aim of the present paper was to analyze the evolution of dosimetric outcomes of cervix BT implants in three Spanish institutions, with respect to EMBRACE II publication.

Material and methods

Dosimetric and volumetric data of cervix BT interventions were collected. All data were obtained from three Spanish hospitals, with which the authors are affiliated. A total of 392 patients were analyzed, including 260 from Institution 1, 72 from Institution 2, and 56 from Institution 3. All patients followed a similar treatment scheme: EBRT followed by 4 MRI-based BT fractions applied in two applicator insertions, 7 Gy per fraction, prescribed according to a GEC-ESTRO biological spread sheet as a compromise between D90 to HR-CTV and IR-CTV, and D2cc to OARs. EBRT component scheme varied according to a patient and Institution, and included 45 Gy in 25 fractions, 50.4 Gy in 28 fractions, 50 Gy in 25 fractions, 52.2 Gy in 29 fractions, 46 Gy in 23 fractions, 48.74 in 24 fractions, and 44.8 Gy in 28 fractions. Most common scheme was 45 Gy delivered in 25 fractions.

This study comprised patients from 2009 until 2019, depending on the data available at each Institution. For each patient, total dose and number of EBRT fractions, D90 of HR-CTV, and D2cc of OARs of BT were obtained. In addition, HR-CTV volume (an average of two BT applications) and number of needles used were also recorded. All three institutions used Elekta BT devices, such as Oncentra TPS (Elekta, Veenendaal, The Netherlands), Utrecht interstitial CT/MR applicator, and HDR-BT afterloader (one Institution had a MicroSelectron v.4, and the other two used Flexion 1.0). Utrecht applicator combines intracavitary and interstitial gynecological BT. 4 and 6 mm diameter intra-uterine tubes, with 15 and 30 degrees curvatures were combined with 15, 20, and 25 mm ovoids, and up to five interstitial plastic needles in each ovoid, with three located in the outer side and two in the inner part, closer to the tandem [20]. Several patients were treated with tandem and ovoids only.

Even though the EMBRACE II protocol was published in 2018, certain institutions had access to the draft versions prior to that date. Not all hospitals could adapt their established protocols at the same time. Institution 1 adapted the EMBRACE II as soon as they obtained access to a draft version at the end of 2016. Institution 2, due to its’ participation in the EMBRACE I clinical trial, could not completely adjust its’ protocol until end of 2017. Institution 3 has still not completely changed the EMBRACE II objectives and constraints. Furthermore, Institution 3 included the sigmoid within delineation of the rectum structure. For this reason, it was assumed that D2cc of the rectum and sigmoid were equal for all patients at this center.

Since the aim of the study was to assess the evolution of dosimetric quality of BT insertions, all dosimetric numbers were compared to the EMBRACE II objective/ tolerance levels for BT component. This protocol was used as a reference since it adds to the state of knowledge regarding local control of tumors and complications in OARs. Therefore, a dose in EQD2 (equivalent total doses in 2 Gy fractions computed using linear-quadratic model, with α/β = 10 Gy for tumor and α/β = 3 Gy for OARs) of EBRT contribution was subtracted from objective/ tolerance values stated at EMBRACE II (Table 1) to obtain objective/tolerance values for BT. It was assumed that both D90 HR-CTV and D2cc of OARs received EBRT prescribed dose.

The equilibrium between dose coverage of HR-CTV and dose of OARs was assessed using index I defined as:

\[
I = \frac{1}{I_{CTV}} \times I_{OAR} = \left( \frac{D_{\text{obj}}^{\text{bladder}}}{D_{\text{obj}}^{\text{bladder}}} - \frac{D_{\text{obj}}^{\text{bladder}}}{D_{\text{obj}}^{\text{rectum}}} \right) \times \left( \frac{D_{\text{2cc,bladder}}^{\text{bladder}}}{D_{\text{2cc,bladder}}^{\text{bladder}}} - \frac{D_{\text{2cc,rectum}}^{\text{rectum}}}{D_{\text{2cc,rectum}}^{\text{rectum}}} \right) \times \left( \frac{D_{\text{2cc,bladder}}^{\text{bladder}}}{D_{\text{2cc,bladder}}^{\text{bladder}}} - \frac{D_{\text{2cc,bladder}}^{\text{bladder}}}{D_{\text{2cc,bladder}}^{\text{bladder}}} \right)
\]

where \(D_{\text{obj}}^{\text{bladder}}\) and \(D_{\text{2cc,bladder}}^{\text{bladder}}\) are the objective doses (in EQD2) for HR-CTV and tolerance levels for different OAR, and \(D_{\text{obj}}^{\text{bladder}}\)
is the upper limit dose for HR-CTV. It should be noted that the objective and tolerated doses refer only to BT component. For example, if EBRT treatment consisted of 45 Gy with 1.8 Gy/fraction (44.25 Gy EQD2\textsuperscript{10} and 43.2 Gy EQD2\textsuperscript{3}), 

\[ D_{90}^{\text{obj}} = 90 \times 44.25 = 405.75 \text{ Gy EQD2}\textsuperscript{10}, \quad D_{90}^{\text{lim}} = 95 \times 44.25 = 422.125 \text{ Gy EQD2}\textsuperscript{10}, \quad D_{90}^{\text{obj}} = 90 \times 43.2 = 388.8 \text{ Gy EQD2}\textsuperscript{3}. \]

According to this definition, the optimal value of index I was 0. There is a critical case, in which 

\[ D_{90}^{\text{obj}} \text{ is equal to } D_{90}^{\text{lim}}, \]

which causes the value of index to be independent of OARs doses. However, with a sufficient decimal precision, this should not occur. In all treatments with 

\[ D_{90} \text{ higher than } D_{90}^{\text{lim}}, \]

the index had a negative value. Moreover, the proportion with OARs was kept within negative range, and treatments with a higher absolute value had a worse assessment. 

\[ D_{90}^{\text{lim}}, \]

which could not be understood as a minimum objective value. Since EMBRACE II established a planning aim of 

\[ D_{90} \text{ between 90 Gy EQD2}\textsuperscript{10} and 95 Gy EQD2\textsuperscript{10}, \]

higher doses within this interval were considered in the present study. Consequently, index I reached its' optimal value, when 

\[ D_{90} = D_{90}^{\text{lim}}, \]

and not when corresponds to 

\[ D_{90}^{\text{obj}}. \]

None of the patients presented with 

\[ D_{90} \text{ of HR-CTV lower than 85 Gy EQD2}\textsuperscript{10}. \]

### Statistical analysis

Statistical analysis of all the dosimetric results was carried out using RStudio software version 1.2.1335. RStudio is an environment for R, a programming language for statistical computing. For those institutions, which have adapted to the EMBRACE II protocol, assessment of statistically relevant differences between two periods (i.e., pre- and post-EMBRACE II) was performed. Depending on distribution of characteristics, Welch, Wilcoxon, or Yuen statistical tests were applied. A p-value of < 0.05 was considered statistically significant.

### Results

Table 2 presents a summary of the analyzed cohort, and a percentage of pure IC and IC/IT techniques in both periods.

Figures 1-3 summarize the values and evolution of 

\[ D_{90}^{\text{obj}} \text{ of HR-CTV, and } D_{2cc}^{\text{obj}} \text{ of OARs for each Institution, normalized by objective or tolerance value for brachytherapy component of the treatment. This means, for example, for a patient who received 43.2 Gy EQD2}\textsuperscript{3} in EBRT, normal-
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...normalization factor of \( D_{2cc} \) rectum would be 21.8 Gy EQD2. However, for the same patient, normalization factor of \( D_{2cc} \) sigmoid would be 26.8 Gy EQD2. In any case, quantities plotted in Figures 1-3 are equal to one, when HR-CTV receives exactly 90 Gy in HR-CTV, 80 Gy in the bladder, 65 Gy in the rectum, and 70 Gy in the sigmoid after the overall treatment. Boxes in these figures represent the 25\(^{th}\) and 75\(^{th}\) percentiles, horizontal line shows the median, and extremes of vertical lines, with 95\% of distribution.

As can be seen in Figure 1, after adapting of EMBRACE II in Institution 1, a conservative approach, increasing the dose to HR-CTV enough to be able to keep OARs almost unchanged, reached a median value of 1.071 for normalized \( D_{90} \). In fact, only \( D_{90} \) was found to present a statistical difference between both periods (\( p_{bladder} = 0.03, p_{rectum} = 0.0004, p_{sigmoid} = 0.02 \)), and delivery of more concentrated HR-CTV dose between objective and upper threshold, as shown in a smaller box in Figure 2. Figure 4 shows an evolution of \( D_{90} \) HR-CTV and \( D_{2cc} \) of the rectum in Institution 2, together with a percentage of interstitial implants with respect to the total number of patients. Since the tolerance limits of OARs were less demanding in the EMBRACE I protocol, distributions of OARs in Figure 3 for Institution 3 were mostly above unity, and distribution of \( D_{90} \) of HR-CTV was below unity.

Index I introduced the above evaluates, with an effect of newly established EMBRACE II objectives having worse values for those treatments with a higher absolute value. Figure 5 and Table 3 represent the distribution of index I for the three centers. A tendency towards higher HR-CTV doses in Institution 2 (Figure 2) was interpreted here as a significant percentage of index I distribution being negative. High doses to OARs (with respect to the
EMBRACE II constraints) of implants in Institution 3 were expressed by index I with higher values. Index I was significantly different only for Institution 1 ($p = 0.0000001$) for the two analyzed periods. Even though the median was not statistically different for Institution 2 ($p = 0.06$), the index I integrated the reduction of variation shown in Figure 2 for both target volume and OARs. Quality of an implant depends on many factors, especially volume of the CTV. The volume of HR-CTV influences the level of conformity and doses to OARs, so that it is possible to achieve without an interstitial component. As can be seen in Figure 6, the equilibrium between $D_{90}$ of HR-CTV and $D_{2cc}$ of OARs was harder to handle for larger CTV volumes, which was expressed by an increase of index I with volume of the tumor.

### Discussion

This study was a retrospective analysis, in which dosimetric information used did not affect patients’ treatments. A total of 392 patients from three Spanish centers, with higher number of cervix BT treatments were analyzed. Most patients were treated from 2012 to 2019. This was a period of numerous developments and published recommendations by international societies. The hypothesis tested was to assess the improvement of both implants and dosimetry planning with time, based on training and experience of both physicians and physicists. The analysis presented in this study showed three different approaches to the above-mentioned adaptation that depended on available resources, adaptation of clinical and optimization protocols, and characteristics of the treated patients among other factors. Institution 1 from the beginning, treated almost all patients with an interstitial component. In this case, the goal was to increase the dose to the tumor while keeping OARs at least as good as in the period of EMBRACE I. Institution 2 evolved from a majority of pure intracavitary implants. The main impact of this change was a statistically significant reduction of doses to OARs depending on the technique used (IC vs. IC/IT; $p_{\text{bladder}} = 0.02$, $p_{\text{rectum}} = 0.003$, $p_{\text{sigmoid}} = 0.03$). Institution 2 sought a maximum allowed dose to CTV, even overreaching this threshold in some patients. The peculiarity of large tumor volume of patients in Institution 3, and the majority of intracavitary implants (Table 2) led to a subtle evolution and difficult equilibrium between $D_{90}$ (coverage of tumor) and OARs. The lack of sufficient interstitial components in an implant of above-average HR-CTV volume, could lead to increased tandem loading, resulting in a more cylindrical dose distribution and increased dose to OARs. As can be expected, those implants with interstitial component led to higher cover-

### Table 3. Summary of index I distribution for all three centers with two analyzed periods. $P$-value between analyzed periods is included with significance for values lower than 0.05

| Institution | Pre-EMBRACE II | Post-EMBRACE II | $p$-value |
|-------------|----------------|-----------------|-----------|
|             | Mean | SD  | Range | Mean | SD  | Range |          |
| 1           | 6    | 7   | -0.1-46.9 | 4    | 8   | -3.1-65.8 | 0.0000001 |
| 2           | -5   | 28  | -100.8-59.0 | 2    | 22  | -34.1-90.3 | 0.06      |
| 3           | 28   | 19  | 1.8-113.9 |       |     |        |          |

![Fig. 6. Dependence of index I with the volume of HR-CTV. Inner graph zooms out the region on volumes lower than 15 cm$^3$](image)

The distribution of HR-CTV volumes published varied between studies. The EMBRACE group has published some studies, which included HR-CTV volume statistics. Jastaniyah et al. [23] presented a volumetric analysis of $GTV_d$ (gross tumor volume at diagnosis) and HR-CTV defined according to GEC ESTRO recommendations. In this case, the reported mean and standard deviation was 31.6 ±16.1 cm$^3$. Recently, the EMBRACE I group [24] reported that HR-CTV mean volume of 1,416 patients was 28 cm$^3$, with 95% confidence interval (20-40 cm$^3$). Also, in Figure 1, an estimated range of 8-117 cm$^3$ is presented [17].

Other studies with HR-CTV volume statistical data have been also published. Cannon et al. showed [25] their results of 2020 audit, in which mean HR-CTV volume was 19.27 cm$^3$ (range, 9.9-29.33 cm$^3$), and Oud et al. [26] reported HR-CTV average volume of 34 patients as 29.4 ±12.5 cm$^3$ (range, 8.5-92 cm$^3$).

A limitation of our study, aiming at index evaluation, was a lack of contouring uncertainty analysis. In Institutions 2 and 3, a single radiation oncologist performs BT treatments, which confirms the absence of inter-observer
variation; on the other hand, in center 1, two radiation oncologists carry out the contouring.

All institutions had a learning and skill curve with regard to the application of interstitial component. Initially, few needles were used, but over time, more and deeper needles were employed not only for enhancing dose conformity to HR-CTV, but also for sparing of OARs. The trend shown in Figure 4 represents this evolution. In Institution 2, significantly lower doses were applied to all OARs when an interstitial component was used ($p_{\text{bladder}} = 0.02$, $p_{\text{rectum}} = 0.003$, $p_{\text{sigmoid}} = 0.03$, $p_{\text{HR-CTV}} = 0.3$). For Institution 3, the opposite results were found; only the coverage of the target volume was significantly different when needles were included ($p_{\text{bladder}} = 0.8$, $p_{\text{rectum}} = 0.3$, $p_{\text{sigmoid}} = 0.3$, $p_{\text{HR-CTV}} = 0.03$). In order to understand the difference in OARs doses between Institutions and for each institution, two relevant points must be considered. On the one hand, threshold doses for OARs present significant variations between the EMBRACE I and EMBRACE II projects, since the former limits were based on historical experience of only a few institutions, and the latter were supported by clinical evidence. Alternatively, the adaptation of each center’s protocol to new guidelines of the EMBRACE II project was not initiated at the same time. New objectives for HR-CTV coverage and OARs sparing could also mean adapting the optimization process and/or the necessity to include more interstitial components in learning process to induce changes.

Index I was used as a metric to illustrate the impact of EMBRACE II in dosimetric outcomes of HDR-BT implants. This index endeavors to assess the equilibrium between HR-CTV coverage and OARs sparing, but not to assess individual plans. However, some limitations must be outlined. There was a critical point in the definition. In those cases, in which $D_{\text{90}}$ equals to $D_{\text{90,lim}}$, the index equals to 0, independently of OARs doses. This situation was always avoided using decimal precision of the treatment planning system (TPS) and Excel sheets applied for radiobiological calculations. This critical point would make the index non-applicable for institutions or specific patients, where treatment was re-normalized in order to equal $D_{\text{90}}$ to $D_{\text{90,lim}}$. It is interesting to analyze individually both terms, i.e., $I_{\text{CTV}}$ and $I_{\text{OAR}}$, as compensation between these two components could occur. However, such compensation was uncommon, since only sub-optimal implants (rare anatomy, lack of interstitial component, etc.) led to low doses and poor coverage of HR-CTV, high OARs doses, or high doses to both, target volume and OARs.

Conclusions

EMBRACE II and ICRU 89 introduced a new paradigm on BT planning towards higher doses to target volumes and OARs better sparing. In order to achieve these new objectives, an increase of interstitial component is needed. However, not all centers had the training or protocol flexibility to adapt to these new guidelines. A total of 392 patients from three Spanish institutions, with a majority of cervix brachytherapy treatments were analyzed. Depending on the local protocol before EMBRACE II, the adaptation was achieved by increasing the interstitial component and the physician and physicist training, which resulted in a significant increase of HR-CTV doses or a reduction of OARs doses. The introduced index I has been able to quantify the evolution of the equilibrium between CTV coverage and OARs sparing, according to EMBRACE II objectives and constraints.

Disclosure

The authors report no conflict of interest.

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