Glenohumeral relationship in maximum elevation

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Introduction

Arm elevation is one of the most important functions of the shoulder in our daily lives [4, 12, 13]. Many studies [1, 3, 5, 7, 9, 11, 14, 16, 17] approached the topics about arm elevation, one [11] of which indicated that the humerus moves toward a similar final position at the end of raising the arm irrespective of the plane of elevation, and its position is one of external rotation and elevation of the humerus relative to the scapula, slightly anterior to the plane of the scapula. However, they only measured rotational angles of the glenohumeral joint and could not clarify the relationships between the anatomical landmarks of its joint. We investigated rotational relationships between the anatomical landmarks of the glenohumeral joint in maximum elevation.

Materials and methods

Twenty-five volunteers (20 men, 5 women) without symptoms or history of shoulder disease were enrolled in the study. Mean age was 29 (21–35) years. All participants provided informed consent. The maximum elevation of the shoulder was defined as the position in which the tips of fingers could reach highest in a standing position. A
surgical mattress (VACUFORM; Schmidt, Garbsen, Germany) made of micro-balls of styrofoam, which could be stabilized by vacuum, was adopted around his or her upper extremity and body to reproduce shoulder position (Fig. 1). The amount of pronation or supination of the forearm was not specified. Each participant maintained the same maximum elevation with that surgical mattress, lying supine in a 0.2-T MRI system (Magnetom Open, Siemens, Munich, Germany). The shoulders were imaged using a three-dimensional (3D) gradient echo (repetition time, 56 ms; echo time, 25 ms; flip angle, 40°) with 2-mm thickness. All images were obtained with an 18-cm FOV and a 256 × 192 matrix. Imaging process required an average of 10 min.

All data were transferred to a computer (O2; SGI, Mountain View, CA) and a 3D image of the glenohumeral joint including the proximal part of the humerus was generated using computer software (3D-Virtuoso, Siemens). Providing instant access to 3D information, the same software allowed anatomies to be viewed from any angle.

Anatomical landmarks such as the glenoidal long axis, glenoid center, humeral head center, and humeral shaft axis (Fig. 2) were defined as described below [10]. On the glenoid rim, the point just posterior to the coracoid base was defined as the superior rim and the point just anterior to the lateral border of the scapula was defined as the inferior rim. The line connecting these points was defined as the glenoidal long axis. The glenoid plane was defined as the plane including the glenoidal long axis, and was parallel to the transverse axis connecting the anterior and posterior rims on a cross-section at the center level of the glenoid. The scapular plane was defined as the plane including the glenoidal long axis and was perpendicular to the glenoid plane.

Two cross-sections of the humerus were obtained at 7.5 and 15 cm from the proximal end. The center for these cross-sections of the cortical bone was determined by fitting a circle, and the humeral axis was defined as the line that passed through the center of these circles. Using the data of Iannotti et al. [8], which showed correlations between size of the glenoid and the radius of curvature of the humeral head, each humeral radius was calculated as follows: \( \text{radius (mm)} = \frac{24 \times \text{length of glenoidal long axis}}{39} \) (where 24 is the average head radius and 39 is the average glenoidal long axis in the population as measured by Iannotti et al.). The head was cut in a plane perpendicular to the humeral axis at the distance of the radius from the proximal end, and the center determined by fitting a circle of the same radius. This was regarded as the center of the head. In this plane, the bottom of the bicipital groove was also plotted.

Fig. 1  a The arm was placed in maximum elevation in which the tips of fingers reached highest in a standing position. A surgical mattress was adopted around his upper extremity and body to reproduce the position. b The mattress is made of micro-balls of styrofoam, which are stabilized by vacuum. c Volunteer with the mattress, lying in oblique supine position in an open MRI (Magnetom Open, Siemens, Germany).
The slope of the humeral long axis on the glenoid was determined by measuring the angle relative to the glenoidal long axis and analyzing their orientation in the transverse plane, relative to the scapular plane, in which the humerus was elevated. Rotation of the glenohumeral joint was visualized on the computer screen as follows. The equator was set on the head surface by the plane parallel to the humeral long axis, including the head center and the bicipital groove. Parallel lines to the equator were analogous to latitudes. Rotation (α) is referenced to latitude by rotating the globe to align longitude including the midpoint (X) of the glenoidal long axis (straight broken line) with the vertical. Meanwhile, the shaft axis and the center of the humerus in each subject were projected orthogonally to the glenoid plane to confirm the relation between the anatomical landmarks.

Ten different glenoids were analyzed measuring length values of the long and the transverse axes by two independent investigators to determine the inter-observer variability. To measure the intra-observer variability, those values in 10 glenoids were measured twice by the same person. Angle values of the plane including the shaft axis and the head center to the equator on the head surface were also analyzed to determine these variabilities for the humerus. All data are expressed as mean ± SD. To assess these variabilities, the interclass and intraclass correlation coefficients were used (Wilcoxon Signed Ranks test).
Results

Variability or reproducibility

Length values of the long and the transverse axes of the glenoid, and angle values of the plane including the shaft axis and the head center to the equator on the head surface were 36.0 ± 3.0 mm, 22.5 ± 2.1 mm, 10.0° ± 8.8°. Those values in ten glenoid and humeral bones showed the variability or the reproducibility was high with a correlation coefficient ranging from 0.73 to 0.98 (Wilcoxon Signed Ranks test) (Table 1).

The humeral shaft showed 102° ± 9° of elevation in the plane which faces 7° ± 8° anterior to the scapular plane on the glenoid. Axial rotation was fixed with the glenoidal long axis parallel to the equator (within 2°).

Figure 3 shows which portion of the head surface the center of the glenoid was located on. It showed the glenoid located on the anterior–superior portion (Zone I) of the head in all subjects.

The humeral head centers and shaft axes projected on the glenoidal plane are shown in Fig. 4. The center of the humeral head projects approximately on the center of the glenoid, showing the humeral head remained centered in the glenoid cavity, and the shaft axes were located above these centers. The same length of axis was projected, and the lengths of their shadows were different between the subjects, indicating the angle of the shaft to the glenoid varied. However, the humeral axis tilted in about the same direction (antero-superiorly) above the center of the glenoid. The direction of the shaft tilting was the same as that of translation from the top of the head to each glenoid location as was mentioned above.

The final position was proved to be the same in all subjects, suggesting this position is unique and may be reached whatever the course of the humerus.

Table 1 Variability or reproducibility

| Variability | Mean ± SD | Mean ± SD | Correlation coefficient |
|-------------|-----------|-----------|-------------------------|
| Length: Glenoidal long axis (mm) | 36.2 ± 23.7 | 36.1 ± 3.5 | 0.98 |
| Length: Glenoidal transverse axis (mm) | 22.6 ± 2.4 | 23.4 ± 2.7 | 0.86 |
| Angle (°) | 12.3 ± 9.0 | 12.5 ± 8.8 | 0.98 |

Reproducibility

| Variability | Mean ± SD | Mean ± SD | Correlation coefficient |
|-------------|-----------|-----------|-------------------------|
| Length: Glenoidal long axis (mm) | 36.2 ± 3.7 | 36.3 ± 3.4 | 0.88 |
| Length: Glenoidal transverse axis (mm) | 22.6 ± 2.4 | 23.9 ± 1.6 | 0.73 |
| Angle (°) | 12.3 ± 9.0 | 13.0 ± 8.4 | 0.95 |

Fig. 3 The centers of the glenoid (black dot) located on the antero–superior portion of the head. The equator (solid line) and the longitude (solid curved line) crossing the top on the equator, divide the head surface into four areas. BG bicipital groove, LT lesser tuberosity, GT greater tuberosity
Discussion

The glenohumeral joint was considered to reach a general position at the end of raising the arm whatever the pass-
way followed by the humerus [4, 6, 11, 13]. However, there has been no precise in vivo description of the glenohumeral joint in maximum elevation. Some discrepancies existed in the past studies about the position of the glenohumeral position in maximum elevation. Browne et al. [3] found that the plane of maximum elevation was 23° anterior to the scapular plane, while Pearl et al. [15] reported the same plane was 4° posterior to the scapular plane. One reason for explaining the discrepancies might be that those studies used different methods. The former was a cadaveric study and the latter study used the scapular locating device for estimating locations of the scapula in vivo. Cadaveric
studies possess limitations in that the scapula is affixed to a support without outer muscles as well as the clavicle and ribs. On the other hand, locating devices have a problem in estimation of location of the bones. Three-dimensional computer-generated MRI without radiation exposure on subjects would be appropriate for analyzing a static position because relations between the bony landmarks can be investigated through trial and error on a computer screen.

For investigating rotational alignment of the joint, we set the equator and its parallel lines on the surface of the humeral head. The equator was determined to include the bicipital groove because several authors [4, 12, 13] suggested its importance to glenohumeral motion or position. In the result, all subjects showed that the glenoidal long axis became parallel to the equator in maximum elevation. As long as axial rotation in the glenohumeral joint is expressed as rotational angle of the humeral axis, those values possibly are varying. One reason for this variation might be that the head has offset and angle of retroversion depends on each subject as was suggested by angle of the plane in Table 1. To the best of our knowledge, this study was the first representing a concrete description about anatomical relationship of rotation in maximum elevation.

Ranges of rotation would be restricted with arm elevation because insertion of the short rotators approaches the glenoid surface and the capsule surrounding the head also becomes tight. Thus, irrespective of the plane of elevation, the shoulder joint would finally converge to the same, i.e., the preferential position. Gagey et al. [6] described behavior of coracohumeral and inferior glenohumeral ligaments that participate in determining the preferential position. In their experimental study, the axis of the humeral shaft in that position was shown to be perpendicular to the glenoid cavity and it also was shown there still existed lateral rotation of the humerus allowing continuation of elevation as a final phase.

Figure 5 illustrated the trajectory of the glenoid on the humeral head during arm elevation. The glenoid moves upward on the surface of the humeral head, converging to the equator with ranges of rotation getting restricted. When the glenoidal long axis becomes parallel to the equator, the glenoid center is located on the top of the head, in which the joint is locked in axial rotation. When the arm is more elevated after that position, the glenoid would only translate to the antero-superior portion (Zone I) of the humeral head without axial rotation.
with rotator cuff tear or without the long head of the biceps might be helpful for clarifying which part of the joint is essential to determine the positioning. Experiments like ex vivo studies simulating rotator cuff tears [2, 18] might also be useful to know the mechanism around maximum elevation.

Even though those limitations should be taken into consideration, the current study might be sufficient to describe the static position of the glenohumeral joint in maximum elevation. The result of the study suggested (a) the position in which the glenoid is on the top of the humeral head with the humeral shaft perpendicular to the glenoid is essentially the final position of elevation, and (b) the humeral axis is slightly anterior to the plane of the scapula and no axial rotation is available for the humerus after that final position. Rehabilitation programs aiming at reaching this position when the joint is impaired after injury or operation would be reasonable from this biomechanical point of view.

Conflict of interest The authors declare that they have no conflict of interest.

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References

1. An KN, Browne AO, Korinek S, Tanaka S, Morrey BF (1991) Three-dimensional kinematics of glenohumeral elevation. J Orthop Res 9:143–149
2. Billuart F, Devun L, Gagey O et al (2007) 3D kinematics of the glenohumeral joint during abduction motion: an ex vivo study. Surg Radiol Anat 29(4):291–295
3. Browne AO, Hoffmeyer P, Tanaka S, An KN, Morrey BF (1990) Glenohumeral elevation studied in three dimensions. J Bone Joint Surg Br 72:843–845
4. Codman EA (1934) The shoulder. Thomas Todd, Boston
5. Freedman L, Munro RR (1966) Abduction of the arm in the scapular plane: scapular and glenohumeral movements. J Bone Joint Surg Am 48:1503–1510
6. Gagey O, Bonfait H, Gillot C, Hureau J, Mazas F (1987) Anatomical basis of ligamentous control of elevation of the shoulder (reference position of the shoulder joint). Surg Radiol Anat 9:19–26
7. Gold GE, Pappas GP, Whalen ST, Cambell G, McAdams TA, Beaulieu CF (2007) Abduction and external rotation in shoulder impingement: an open MR study on healthy volunteers—initial experience. Radiology 244:815–822
8. Iannotti JP, Gabriel JP, Schneck SL, Evans BG, Misra S (1992) The normal glenohumeral relationships. An anatomical study of one hundred and forty shoulders. J Bone Joint Surg Am 74:491–500
9. Inman VT, Saunders JB, Abbott LC (1944) Observation on the function of the shoulder joint. J Bone Joint Surg Am 26:1–30
10. Inui H, Sugamoto K, Miyamoto T, Yoshikawa H, Machida A, Hashimoto J, Nobuhara K (2002) Three-dimensional relationship of the glenohumeral joint in the elevated position in shoulders with multidirectional instability. J Shoulder Elb Surg 5:510–515
11. Ludewig PM, Phandke V, Braman J, Hassett DR, Cieminski CJ, LaPrade RF (2009) Motion of the shoulder complex during multiplanar humeral elevation. J Bone Joint Surg Am 91:378–389
12. Matsen FA III, Titleman RM, Lippitt SB, Rockwood CA Jr, Wirth MA (2003) Glenohumeral instability. In: Rockwood CA Jr, Matsen FA III, Wirth MA, Lippitt SB (eds) The shoulder, 3rd edn. WB Saunders, Philadelphia, pp 655–794
13. Nobuhara K (2003) Biomechanics of the shoulder. In: Nobuhara K (ed) The shoulder: its function and clinical aspects. World Scientific, Singapore, pp 49–91
14. Ogston JB, Ludewig PM (2007) Differences in 3-dimensional shoulder kinematics between persons with multidirectional instability and asymptomatic controls. Am J Sports Med 35:1361–1370
15. Pearl ML, Jackins S, Lippitt SB, Sidles JA, Matsen FA III (1993) Humeroascapular positions in a shoulder range-of-motion-examination. J Shoulder Elb Surg 6:296–305
16. Poppen NK, Walker PS (1976) Normal and abnormal motion of the shoulder. J Bone Joint Surg Am 58:195–201
17. Stokdijk M, Eilers PHC, Nagels J, Rozing PM (2003) External rotation in the glenohumeral joint during elevation of the arm. Clin Biomech 18:296–302
18. Tetreault P, Levasseur A, Lin JC, Lin JC, de Guise J, Nuno N, Hagemeister N (2011) Passive contribution of the rotator cuff to abduction and joint stability. Surg Radiol Anat 33(9):767–773