Research Article

Evaluation of Antimicrobial and Antibiofilm Activities of Copper Oxide Nanoparticles within Soft Denture Liners against Oral Pathogens

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Received 13 March 2021; Revised 26 April 2021; Accepted 26 May 2021; Published 4 June 2021

Academic Editor: Guillermo Mendoza-Diaz

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Objectives. Soft denture liners provide a favorable environment for adhesion and colonization of microorganisms. This in vitro study aimed to examine the efficacy of different concentrations of copper oxide nanoparticles (CuO NPs) incorporation into soft denture liner on the biofilm formation of the microbial species.

Methods. Field Emission Scanning Electron Microscopy (FESEM) images from NPs were recorded. Antifungal susceptibility testing of CuO NPs against five standard strains of Candida albicans (CBS 10261, 1905, 1912, 1949, 2730), Streptococcus mutans (ATCC35668), Streptococcus sobrinus (ATCC27607), and Streptococcus salivarius (ATCC9222) was performed by the broth microdilution method with the Clinical and Laboratory Standards Institute reference method. The biofilm inhibition percentages of CuO NPs on the soft denture liners were determined by XTT assay.

Results. The characterization of CuO NPs by scanning electron microscope (SEM) analyses confirmed the synthesis of NPs with appropriate structure and size with a mean diameter of 18.3 ± 9.1 nm. The CuO NPs successfully inhibited the growth of the tested standard strains of C. albicans and Streptococcus spp. at concentrations ranging from 64 to 128 µg mL⁻¹. Indeed, incorporation of CuO NPs at a concentration of 500 µg mL⁻¹ into the soft denture liners exhibited a significant activity (75%) in inhibition of C. albicans. Biofilm formation in a dose-dependent manner. The biofilm formation of C. albicans in the presence of CuO NPs was lower than Streptococcus spp. in comparison with the control group (p < 0.05). Conclusion. Incorporation of CuO NPs significantly decreased the colonization and plaque formation of the oral pathogens, especially C. albicans accumulation. These NPs may be useful as a promising agent for the antimicrobial management of soft denture liner materials.

1. Introduction

Soft denture liners are resilient materials that are used as a shock absorber under the denture, to reduce the functional loads to the bearing mucosa by distributing the loads homogeneously on the denture-bearing tissues [1]. This is mainly useful in patients with sharp or atrophic ridges having a low tolerance to the loads applied by the dentures. They are also commonly used for conditioning the irritated tissues mostly induced by ill-fitted dentures. Soft denture liners are prone to easy deterioration, which increases the surface roughness. It will result in an increase in susceptibility to colonization and growth of the microorganisms. Studies have shown that fungal and bacterial microorganisms initially adhere to the surface of the lining and accumulations on the appliances [2–4]. In the oral cavity, most
colonizing and infecting microorganisms are found not as single-living cells, but rather as complex structured microbial communities, often encapsulated within a matrix of exopolymeric material, and attached to biotic or abiotic surfaces. These communities are referred to as biofilms [5, 6]. Microbial biofilms are 3D structures that have gained the ability to resist antimicrobials and immune cell challenges. It is noteworthy that environmental conditions under the denture as well as the structure of materials supported this microbial growth and played a key role in denture-related stomatitis [7, 8]. Denture stomatitis is a common disease in denture wearers (15–70%) which mainly contributes to Candida spp. and oral bacteria [6, 9]. On the other hand, for some elderly patients with some physical and mental disabilities, conventional chemical and mechanical denture cleansing procedures are challenging [10].

Moreover, some of the mentioned cleansing methods can also damage the soft denture liners and cause more microbial plaque accumulation [11, 12]. Several researchers have already incorporated a variety of medicament including antifungal drugs, metal oxides, and herbs into the soft denture liners, as a reliable method to overcome denture-induced stomatitis [13, 14]. Although many of these modified soft denture liners showed promising results against microorganisms, different shortcomings were also reported for the investigated additives. For example, there was no certain durability and robustness of the effective dose for the evaluated additives. Some of these soft denture liners were reported to be effective only for a short time (3–7 days) [4, 15]. Some other studies demonstrated that some of these antifungal additives compromise the mechanical properties of the soft denture liners [16, 17]. Although the beneficial effect of antimicrobial additives to the soft denture liners has been proved, no antimicrobial soft liner is commercially available, yet. Nanotechnology has numerous modern applications in the field of dentistry, including disease diagnosis, therapy, and prevention. Restorative dentistry, cancer diagnosis and treatment, implant dentistry, and molecular imaging are some examples of the application areas [18]. Nanomaterials are natural or manufactured materials containing particles in the size ranges of 1–100 nm [19]. Recently, copper oxide nanoparticles (CuO NPs) have been extensively used in different areas of science and technology due to their good thermal, electrical conductivity, and low cost [20]. Previous studies have demonstrated that the incorporation of NPs in orthodontic brackets and alginate significantly reduces the amount of microbial biofilm [21, 22]. Recently, in order to reduce both the cost and the toxicity of CuO NPs, biological sources such as plants have been used instead of chemical methods, which have shown an additional antibacterial activity, as well [23–25].

To the best of our knowledge, there is still no report about the antimicrobial and antibiofilm activity of the CuO NPs incorporated into the soft liner in different concentrations. Therefore, this study aimed to evaluate the effectiveness of incorporating CuO NPs into the soft liner and assess its antimicrobial and antibiofilm activity effects against Streptococcus mutans, Streptococcus sobrinus, Streptococcus salivarius, and Candida albicans.

2. Materials and Methods

2.1. Synthesis and Characterization of CuO NPs. Briefly, 25 mL ethanolic solution of copper acetate (Merck, Germany, 0.2 mol L⁻¹) was mixed with 25 mL ethanolic solution of sodium hydroxide (Merck, Germany, 0.4 mol L⁻¹) by a magnetic stirrer followed by the addition of 0.5 g polyethylene glycol (molecular weight, 20,000) (Merck, Germany). The mixture was then refluxed for 25 min. A brown precipitate was obtained that was washed several times by absolute ethanol and acetone. The sample (CuO NPs) was dried at room temperature. Besides, Field Emission Scanning Electron Microscopy (FESEM) images from NPs were recorded using a TESCAN Mira 3-XMU (Czech Republic).

2.2. Preparation of Resin Disks Containing Different Concentrations of CuO NPs. In this study, we used a self-cured acrylic-based soft liner (GC Cooperation, Tokyo, Japan) which consists of powder and liquid. According to the manufacturer’s instructions, experimental soft denture liner discs (10.0 × 3.0 mm) were fabricated containing 0, 0.5, 5, 50, and 500 μg mL⁻¹ concentrations of CuO NPs. After CuO NPs incorporation, the prob sonication (soniprep-150, England) was used for 3 minutes to disperse the mixture. Afterward, the powder and liquid were mixed placed in a disk-shaped silicone mold, pressed between two glass slabs until the soft denture liner cured, and then polished. A total of 80 discs were prepared and divided into five groups (n = 16) according to the concentration of CuO NPs incorporated. Then, within a group, four soft denture liner discs were assigned to each strain.

2.3. Disinfection of the Specimens. The specimens were disinfected by immersing in glutaraldehyde 2% for 2 min and rinsed with sterile water.

2.4. Antimicrobial Susceptibility Tests. The antimicrobial activity of CuO NPs against five standard strains of Candida albicans (CBS 10261, 1905, 1912, 1949, 2730), Streptococcus mutans (ATCC35668), S. sobrinus (ATCC27607), and S. salivarius (ATCC29222) was determined. Standard strains of bacteria and C. albicans were seeded on the brain heart infusion agar and Sabouraud dextrose agar (Merck, Germany), respectively. Then, the culture plates were incubated at 35 ± 2°C between 18 and 24 h. Minimum inhibitory concentration (MIC) of CuO NPs was determined by the broth microdilution method as recommended by the clinical and laboratory standards institute (CLSI), in the range of 0.5 μg mL⁻¹–512 μg mL⁻¹.

Briefly, RPMI-1640 medium (with L-glutamine and phenol red, without bicarbonate, Sigma, USA) was prepared and buffered at pH 7.0 with 0.165 mol 3-(N-morpholino) propane sulfonic acid (MOPS) (Sigma-Aldrich, Steinheim, Germany). Serial dilutions of NPs (0.5 to 512 μg mL⁻¹) were prepared in 96-well microtitre trays using RPMI-1640 buffered with MOPS. Stock inoculums were prepared by
suspending three colonies of the examined bacteria and
C. albicans in 5 mL sterile 0.85% NaCl and adjusting the
turbidity of the inoculums to 0.5 McFarland standards at
530 nm wavelengths (this yields stock suspension of
1–5 × 10^8 cells mL^-1). Working suspension for C. albicans
and bacteria was prepared by making 1/1000 and 1/100
dilutions, respectively, with broth media of the stock sus-
pension. After the addition of 0.1 mL of the C. albicans and
bacteria inoculums to the wells, the trays were incubated at
30°C for 24 h in a humid atmosphere. The uninoculated
medium was included as a sterility control (blank). Besides
growth controls, media with inoculums but without NPs
were included. The growth in each well was compared with
that of the growth control well. MICs were visually deter-
mined and defined as the lowest concentration of NPs that
completely inhibited the growth of standard strains of
bacteria and C. albicans [8].

2.5. Determining the Antibiofilm Activity

2.5.1. Biofilm Preparation and Growth. For biofilm devel-
opment, C. albicans (CBS 10261) strains were cultured in
Sabouraud dextrose agar (Merck, Germany) medium while
S. mutans (ATCC35668), S. sobrinus (ATCC27607), and S.
salivarius (ATCC9222) were cultured in the brain heart
infusion (BHI) (Merck, Germany) agar. After 24 h, one loop
of C. albicans and bacteria strains colonies were transfered
to 20 mL Sabouraud dextrose and brain heart infusion broth
(Merck, Germany), respectively, and incubated at 30°C over-
night in an orbital shaker (shaken at 100 rpm). Candida albicans and bacteria cells were then harvested and washed
twice in sterile phosphate-buffered saline (PBS, 0.8% w/v),
sodium chloride (0.02% w/v, Merck, Germany), KH₂PO₄
(0.31% w/v, Merck, Germany), Na₂HPO₄·12H₂O (0.02% w/v,
Merck, Germany), and KCl (Panreac, Madrid, Spain). After-
wards, a suspension of respective microorganisms was pre-
pared in RPMI-1640 medium buffered with MOPS [3-(N-
morpholino) propane sulfonic acid]. C. albicans stocks
were used to prepare microbial suspension with 0.15 optical
densities at 530 nm. This turbidity is equal to 1 × 10^8 yeasts mL^-1.
All bacteria suspension with an optical density of 0.1 at 530 nm
was also prepared. This turbidity is equal to 1.5 × 10^8 CFU
mL^-1. Soft denture liner disks containing different concentra-
tions of CuO NPs were then placed as pairs in sterile 12-well
cell culture plates. One mL of microbial suspension was added
to each well; then, the plates were placed at 30°C for 48 h to
form a biofilm [26].

2.5.2. Assessing Biofilm Formation. Biofilm formation was
assayed by using a 2,3-bis(2-methoxy-4-nitro-5-sulfo-phen-
yl)-2H-tetrazolium-5-carbox-anilide (XTT, Sigma, USA)
reduction assays. XTT was prepared as a saturated solution
at a concentration of 0.5 mg mL^-1 in Ringer’s lactate. This
solution was filter-sterilized through a 0.22 μm pore size
filter, divided into aliquots, and then stored at −70°C. Prior to
each assay, an aliquot of the XTT stock solution was thawed,
and treated with menadione sodium bisulfite (Sigma, USA,
10 mmol L^-1 prepared in distilled water) to obtain the final
concentration of 1 μmol L^-1 of menadione. After 48 h, the
plates were brought out of the incubator, and the contents of
each well were emptied. Plates were washed with PBS three
times for the unattached microorganisms to be extracted
from the plates. In the next phase, acrylic discs were gently
transferred to new plates. A 500 μL aliquot of XTT-menadione
was then added to each pre-washed biofilm and the
wells that contained a disk treated with CuO NPs and in-
cubated for 4 h at 35°C in dark to measure the background
XTT levels. Finally, the content of the wells was transferred
to another plate and their spectral absorbance at a wave-
length of 570 nm was evaluated by a multi-well scanning
spectrophotometer (Polar star omega, Germany). All trials
were performed in duplicate to reduce the error rate as much
as possible. The well containing soft liner disks and culture
medium without microorganism was considered as the
negative control and soft liner disks in the wells containing
media and organism were used as the positive control [26].

2.6. Statistical Analysis. Statistical analysis was performed
using SPSS software (version 11.0) and Mann–Whitney U
test was used to compare the microbial biofilm formation
between the control and each tested concentrations groups.
The quantitative data were presented in terms of mean and
standard deviations and p value <0.05 was considered as the
significance level threshold.

3. Results

Characterization of CuO NPs by SEM analyses confirmed
the synthesis of NPs with appropriate structure and size.
Figure 1 shows FESEM images recorded from CuO NPs at
different magnifications. The lungs of the particles are
observed in the low-magnified image, and at higher mag-
nifications, the adhered NPs of CuO are observed. A mean
diameter of 18.3 ± 9.1 nm (n = 50) was obtained for NPs.

Antifungal and antimicrobial test results are presented in
Table 1. CuO NPs successfully inhibited the growth of the
tested standard strains of C. albicans and bacteria at con-
centrations ranging from 64 to 128 μg mL^-1 (geometric
mean = 84.44 μg mL^-1).

Moreover, biofilm formation of C. albicans (CBS 10261)
and Streptococcus spp. in the presence of CuO NPs with 0.5,
5, 50, and 500 μg mL^-1 were measured quantitatively by the
XTT reduction assay and the results are presented in Table 2.

The results indicated that CuO NPs exhibited a signific-
ant activity in inhibition of microbial biofilm formation in
a dose-dependent manner, as reflected by lower absorbance
reading when compared with the untreated control. Indeed,
the Candida biofilm formation was inhibited by up to 75% at
the concentration of 500 μg mL^-1 of CuO NPs. The biofilm
formation of C. albicans in the presence of CuO NPs was
significantly lower than Streptococcus spp. biofilm formation
with a statistically significant difference (p < 0.05).

4. Discussion

Copper oxide is one of the copper compound families that
exhibit useful physical properties, such as high-temperature
superconductivity, electron correlation effects, and spin dynamics. It is relatively cheap, easily mixed with polar liquids and polymers, and comparatively stable in terms of chemical and physical activities. It is notable that the considerable antimicrobial effect of CuO NPs was achieved in previous studies [27, 28].

Intrinsic porosity in the soft denture liners makes them susceptible to be colonized by microorganisms. Microorganisms form a biofilm surface over the prosthesis in contact with oral tissue and may manifest as cracks and irregularities that occur in some stages of soft denture liner preparation. These defects can act as oral reservoirs for adhesion and colonization of microorganisms, which include *C. albicans* and *Streptococcus* species particularly, *S. mutans*, *S. sobrinus*, and *S. salivarius* [29, 30].

*Candida albicans* has the most important and predominant oral fungal pathogen. It can adhere and proliferate upon both soft and hard tissue surfaces within the oral cavity, and form biofilm. *Streptococcus mutans* is a major pathogen of dental caries that can cause significant health problems for denture wearers [26].

Due to some disadvantages of direct use of NPs including the objectionable taste of some additives and the necessity of frequent utilization that needs patient cooperation [31], the purpose of the present study was to assess the antimicrobial and antibiofilm effects of CuO NPs (in the mean diameter of 18.3 ± 9.1 nm) incorporated into soft denture liners.

In this study, CuO NPs inhibited the growth of *C. albicans* and oral *Streptococcus* spp. at a geometric means
of 84.44 μg mL⁻¹. It is noteworthy that the microbial inhibition efficacy of NPs depends on their concentration as well as their size and shape. Khan et al. found that CuO NPs at 50 μg mL⁻¹ concentration significantly prevented the growth of some oral bacteria [32] and the MIC values of this study were comparable to the present study. Sathiyavimal et al. showed that non-toxic chitosan coated CuO NPs have a good inhibitory effect against specially Gram-negative bacteria rather than Gram-positive ones, at the concentration of 20–80 μg mL⁻¹ [24].

In this work, the antibiofilm activity of CuO NPs exhibited various effects against different microorganisms. In the current study, incorporating the CuO NPs in soft denture liner samples inhibited the biofilm formation of *C. albicans* and oral *Streptococcus* species in a dose-dependent manner. The bioactivity and biofilm formation of *C. albicans* and *Streptococcus* spp. successively decreased with increasing CuO NPs concentration by using XTT reduction assays. The MIC and biofilm formation results can probably explain the anti-adhesion and subsequently the antibiofilm effects of CuO NPs.

In all four concentrations of 0.5, 5, 50, and 500 μg mL⁻¹ of CuO NPs that were incorporated in soft denture liners, antibiofilm effects were shown in comparison to the control group, but it was not significant at lower concentrations of 0.5 and 5 μg mL⁻¹.

It seems that incorporating CuO NPs in low concentrations probably does not release and interfere in adhesion and biofilm formation. Based on our findings, there was 75% *C. albicans* biofilm inhibition at 500 μg mL⁻¹ of CuO NPs concentration. These findings were in the same line as those of Sivaraj et al. [33].

Among the bacterial species, *S. sobrinus* had the lowest rate (37%) of biofilm formation at 500 μg mL⁻¹ of CuO NPs, while *S. mutans* and *S. salivarius* were less susceptible species to CuO NPs (70% and 40% biofilm formation at 500 μg mL⁻¹, respectively).

The structure of the cell wall plays an important role in the tolerance or susceptibility of the microorganism in the presence of metal NPs. Based on previous findings, *Streptococcus* strains, as Gram-positive bacteria have a large cell wall, with multiple layers of peptidoglycan, and other protective surface structures [34, 35].

Based on the current study, soft denture liner containing 0.5, 5, and 50 μg mL⁻¹ CuO NPs had no significant effect on *Streptococcus* spp. adhesion and, subsequently, biofilm formation (p value > 0.05). These findings were in contrast with Eshed et al. study, indicating that CuO NPs at low concentration prevented the biofilm formation of *S. mutans* [36]. The possible explanation for these differences may be related to biofilm formation assay. In the present study, the XTT method was used as a quantitative measurement of biofilm formation.

The results of this microbial assay confirmed that the susceptibility of *C. albicans* to CuO NPs of the soft denture liner samples was more than oral *Streptococcus* strains. These findings were consistent with Méndez-Serrano’s study [37].

In another study, the evaluation of *candidal* biofilm formation on the teeth coated with CuO NPs revealed the reduction of biofilm formation by 70% which is in line with the result of the present study [36]. In a study by Pugazhendhi et al., it was shown that Fe doped CuO has a very good antimicrobial and antibiofilm activity against *S. aureus*, *S. epidermidis*, and *C. albicans*. Due to its cationic nature, it would have promoted an easy binding and penetration, which leads to a fungicidal activity [38].

As revealed in another study, coated brackets with metal NPs showed dramatic antimicrobial and antibiofilm effects in comparison with the control groups [21]. The antimicrobial mechanisms of CuO NPs may be related to microbial cell wall attachment, and cause structural changes, which then provokes intracellular oxidative stress. Consequently, they reduce the vital activity of the microbial cell such as permeability, which then results in less biofilm formation activity and eventually leads to the death of the pathogens.

In a study, Tabrez Khan et al. found that 50 μg mL⁻¹ of CuO NPs (40 nm) prevented the growth of some oral bacteria [39]. The MIC values of this study were comparable to ours, although the size of our NPs was smaller (18 nm) than theirs.

Further studies are recommended to assess the biocompatibility and mechanical properties of denture liners containing CuO NPs, especially at MIC concentration. The stability and duration of the effectiveness of denture liners containing CuO NPs should be assessed. It is also suggested that the mechanism of antimicrobial effect of CuO NPs in different strains of fungi and bacteria should be evaluated in the future.

### 5. Conclusion

It was concluded that the CuO NPs incorporated soft denture liner is an efficient, practical, and accessible alternative for denture users with an oral microbial infection. The CuO NPs might have the potential as a microbial resistant coating in biomedical devices and limit the spread of some pathogenic microbes.

### Data Availability

All the data used to support the findings of this study are available from the corresponding author upon request.

### Additional Points

Scientific rationale for study: the use of soft denture liners is associated with several problems such as difficulty in cleaning, microbial colonization, and subsequently caused denture stomatitis. In old patients, cleansing procedures are challenging and make soft liners susceptible to plaque accumulation. To reduce this problem, several solutions such as adding NPs have been suggested. Principal findings: CuO NPs caused a significant reduction of microbial growth and incorporation of these NPs in soft denture liner decreased biofilm formation. Practical implications: the soft denture liner with CuO NPs is proposed as an appropriate carrier for the prevention of denture stomatitis and improves their properties.
Conflicts of Interest

The authors declare that they have no conflicts of interest regarding the publication of this paper.

Authors’ Contributions

K. Z. and E. A. conceived the ideas; N. S and H. H collected the data; Z. Z and E. A. analyzed the data; and K. Z., E. A., and Z. Z. led the writing.

Acknowledgments

This study was financially supported by the Vice-Chancellor for Research of Shiraz University of Medical Sciences (Grant Agreement No. 11571). The authors wish to thank Dr. Nasrin Shokrpour at the Research Consultation Center (RCC) of Shiraz University of Medical Sciences for his invaluable assistance in editing this manuscript.

References

[1] H. S. A. Alshakaki and H. A. Al-Essa, “A comparative evaluation of shear bond strength between self-cured resilient liner and denture base resin with different surface treatments,” International Journal of Applied Dental Sciences, vol. 6, 2020.

[2] C. B. Melo, “Effect of a continuous mechanical polishing protocol on the color stability microhardness mass and surface roughness of denture base acrylic resin,” The Journal of Prosthetic Dentistry, in Press, 2020.

[3] S. An, “Incorporation of antimicrobial agents in denture base resin: a systematic review,” The Journal of Prosthetic Dentistry, 2020, in Press.

[4] A. Fallah-tafti, “Stability and duration of antifungal effects of Nystatin and Fluconazole mixed with a tissue conditioner on colonization of Candida Albicans (in vitro),” Journal of Research in Dental Sciences, vol. 11, no. 1, pp. 21–26, 2014.

[5] K. M. Lyons, R. D. Cannon, J. Beumer, M. M. Bakr, and R. M. Love, “The role of biofilms and material surface characteristics in microbial adherence to maxillary obturator materials: a literature review,” The Cleft Palate-Craniofacial Journal, vol. 57, no. 4, pp. 487–498, 2020.

[6] K. R. Pachava, L. K Nadendla, L. S Alluri, H Taheen, and N. P Saja, “In vitro antifungal evaluation of denture soft liner incorporated with tea tree oil: a new therapeutic approach towards denture stomatitis,” Journal of Clinical and Diagnostic Research: JCDR, vol. 9, no. 6, pp. ZC62–4, 2015.

[7] L. Karygianni, “Biofilm matrixome: extracellular components in structured microbial communities,” Trends in Microbiology, vol. 28, no. 8, pp. 668–681, 2020.

[8] Z. Zareshahrabadi, “Morphogenesis and pathogenesis regulation of Candida albicans by probiotic bacterium - pediococcus acidilactici,” Journal of Microbiology, Biotechnology and Food Sciences, vol. 10, no. 1, pp. 5–11, 2020.

[9] M. Mundathaje, “Redefining treatment for denture stomatitis—a review,” International Journal of Research In Dentistry, vol. 4, no. 2, pp. 8–20, 2014.

[10] M. I. Issa and N. Abdul-Fattah, “Evaluating the effect of silver nanoparticles incorporation on antifungal activity and some properties of soft denture lining material,” Journal of Baghdad College of Dentistry, vol. 325, no. 2219, pp. 1–15, 2015.

[11] F. Mahboub, F. Saleshaber, F. Parnia, V. Gharekhani, Y. Kananzadeh, and M. Taghizadeh, “Effect of denture cleansing agents on tensile and shear bond strengths of soft liners to acrylic denture base,” Journal of Dental Research, Dental Clinics, Dental Prospects, vol. 11, no. 3, pp. 183–188, 2017.

[12] H. S. Mohammed, S Singh, P. A Hari et al., “Evaluate the effect of commercially available denture cleansers on surface hardness and roughness of denture liners at various time intervals,” International Journal of Biomedical Science: IJBS, vol. 12, no. 4, pp. 130–142, 2016.

[13] V. T. Noronha, A. J. Paula, G. Duran et al., “Silver nanoparticles in dentistry,” Dental Materials, vol. 33, no. 10, pp. 1110–1126, 2017.

[14] Z. Yang, L. Han, Y. Guo, L. Jia, C. Yin, and Y. Xia, “Nano-technology in dental therapy and oral tissue regeneration,” in Nanotechnology in Regenerative Medicine and Drug Delivery Therapy, Springer, Singapore, pp. 91–189, 2020.

[15] J. A. Skupien, F. Valentini, N. Boscasto, and T. Pereira-Cenci, “Prevention and treatment of Candida colonization on denture liners: a systematic review,” The Journal of Prosthetic Dentistry, vol. 110, no. 5, pp. 356–362, 2013.

[16] S. Sathiyavimal, S. Vasantharaj, V. Veeramani et al., “Green chemistry route of biosynthesized copper oxide nanoparticles using Pidium guaiava leaf extract and their antibacterial activity and effective removal of industrial dyes,” Journal of Environmental Chemical Engineering, vol. 9, no. 2, Article ID 105033, 2021.

[17] V. M. Urban, T. F. Lima, M. G. Bueno et al., “Effect of the addition of antimicrobial agents on shore A hardness and roughness of soft lining materials,” Journal of Prosthodontics, vol. 24, no. 3, pp. 207–214, 2015.

[18] L. K. Foong, M. M. Foroughi, A. F. Mirhosseini et al., “Applications of nano-materials in diverse dentistry regimes,” RSC Advances, vol. 10, no. 26, pp. 15430–15460, 2020.

[19] S. R. D’Mello, C. N. Cruz, M.-L. Chen, M. Kapoor, S. L. Lee, and K. M. Tyner, “The evolving landscape of drug products containing nanomaterials in the United States,” Nature Nanotechnology, vol. 12, no. 6, pp. 523–529, 2017.

[20] A. A. Alswat, M. B. Ahmad, M. Z. Hussein, N. A. Ibrahim, and T. A. Saleh, “Copper oxide nanoparticles-loaded zeolite and its characteristics and antibacterial activities,” Journal of Materials Science & Technology, vol. 33, no. 8, pp. 889–896, 2017.

[21] B. Ramazanzadeh, A Jahanbin, M Yaghoubi et al., “Comparison of antibacterial effects of ZnO and CuO nanoparticles coated brackets against Streptococcus mutans,” Journal of Dentistry ( Shiraz, Iran), vol. 16, no. 3, pp. 200–5, 2015.

[22] K. Ginjupalli, R. Alla, T. Shaw, C. Tellapragada, L. Kumar Gupta, and P. Nagaraja Upadhy, “Comparative evaluation of efficacy of Zinc oxide and Copper oxide nanoparticles as antimicrobial additives in alginate impression materials,” Materials Today: Proceedings, vol. 5, no. 8, pp. 16258–16266, 2018.

[23] S. Sathiyavimal, S. Vasanthiraj, D. Bhariath et al., “Biogenesis of copper oxide nanoparticles (CuONPs) using Sida acuta and their incorporation over cotton fabrics to prevent the pathogenicity of Gram negative and Gram positive bacteria,” Journal of Photochemistry and Photobiology B: Biology, vol. 188, pp. 126–134, 2018.

[24] S. Sathiyavimal, S. Vasanthiraj, T. Kaliannan, and A. Pugazhendi, “Eco-biocompatibility of chitosan coated biosynthesized copper oxide nanocomposite for enhanced industrial (Azo) dye removal from aqueous solution and...
antibacterial properties,” *Carbohydrate Polymers*, vol. 241, Article ID 116243, 2020.

[25] S. Vasantharaj, S. Sathiyavimal, M. Saravanan et al., “Synthesis of ecofriendly copper oxide nanoparticles for fabrication over textile fabrics: characterization of antibacterial activity and dye degradation potential,” *Journal of Photochemistry and Photobiology B: Biology*, vol. 191, pp. 143–149, 2019.

[26] A. Azad, “Protective effects of the probiotic bacterium Streptococcus thermophilus on Candida albicans morphogenesis and a murine model of oral candidiasis,” *Iranian Journal of Medical Sciences*, vol. 46, no. 3, pp. 207–217, 2020.

[27] M. I. Din, “Single step green synthesis of stable copper oxide nanoparticles as efficient photo catalyst material,” *Biomedical Materials*, vol. 9, pp. 41–48, 2017.

[28] P. G. Bhavyasree and T. S. Xavier, “Green synthesis of Copper Oxide/Carbon nanocomposites using the leaf extract of Adhatoda vasica Nees, their characterization and antimicrobial activity,” *Heliyon*, vol. 6, no. 2, Article ID e03323, 2020.

[29] M. I. A. Arbel´aeza, “Long-term effect of daily chemical dis-infection on surface topography and Candida albicans biofilm formation on denture base and reline acrylic resins,” *Oral Health and Preventive Dentistry*, vol. 18, pp. 999–1010, 2020.

[30] J. B. Pinheiro, M. P. Vomero, C. do Nascimento et al., “Genomic identification of microbial species adhering to maxillofacial prostheses and susceptibility to different hygiene protocols,” *Biofouling*, vol. 34, no. 1, pp. 15–25, 2018.

[31] R. K. Alla, “evaluation of the antimicrobial activity of heat-cure denture base resin materials incorporated with silver nanoparticles,” *International Journal of Dental Materials*, vol. 1, 2019.

[32] M. Ahamed, “Synthesis characterization and antimicrobial activity of copper oxide nanoparticles,” *Journal of Nanomaterials*, vol. 2014, Article ID 637858, 4 pages, 2014.

[33] R. Sivaraj, P. K. S. M. Rahman, P. Rajiv, S. Narendran, and R. Venkatesh, “Biosynthesis and characterization of Acalypha indica mediated copper oxide nanoparticles and evaluation of its antimicrobial and anticancer activity,” *Spectrochimica Acta Part A: Molecular and Biomolecular Spectroscopy*, vol. 129, pp. 255–258, 2014.

[34] H. M. Yusof, R. Mohamad, and U. H. Zaidan, “Microbial synthesis of zinc oxide nanoparticles and their potential application as an antimicrobial agent and a feed supplement in animal industry: a review,” *Journal of Animal Science and Biotechnology*, vol. 10, no. 1, pp. 1–22, 2019.

[35] L. Pasquina-Lemonche, J. Burns, R. D. Turner et al., “The architecture of the gram-positive bacterial cell wall,” *Nature*, vol. 582, no. 7811, pp. 294–297, 2020.

[36] M. Eshed, J. Lellouche, S. Matalon, A. Gedanken, and E. Banin, “Sonochemical coatings of ZnO and CuO nanoparticles inhibit Streptococcus mutans biofilm formation on teeth model,” *Langmuir*, vol. 28, no. 33, pp. 12288–12295, 2012.

[37] J. M´endez-Serrano, “Adhesion of Candida albicans and Streptococcus mutans to silver nanoparticle-modified polymethylmethacrylate,” *Interciencia*, vol. 45, no. 1, pp. 23–27, 2020.

[38] A. Pugazhendhi, S. S. Kumar, M. Manikandan, and M. Saravanan, “Photocatalytic properties and antimicrobial efficacy of Fe doped CuO nanoparticles against the pathogenic bacteria and fungi,” *Microbial Pathogenesis*, vol. 122, pp. 84–89, 2018.

[39] S. Tabrez Khan, M. Ahamed, A. Al-Khedhairy, and J. Musarrat, “Biocidal effect of copper and zinc oxide nanoparticles on human oral microbiome and biofilm formation,” *Materials Letters*, vol. 97, pp. 67–70, 2013.