Research Article

Evaluation of Fracture Toughness, Color Stability, and Sorption Solubility of a Fabricated Novel Glass Ionomer Nano Zirconia-Silica-Hydroxyapatite Hybrid Composite Material

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The aim of this study was to investigate the effects of adding a nano zirconia-silica-hydroxyapatite (nanoZrO₂-SiO₂-HA) composite synthesized using a one-pot sol-gel technique to a conventional glass ionomer cement (GIC), which was then characterized using X-ray diffraction (XRD). Following the characterization studies, further investigations were carried out after the addition of nanoZrO₂-SiO₂-HA to cGIC (GIC nanoZrO₂-SiO₂-HA) at various percentages (~5% to 9%) to compare their fracture toughness, color stability, and sorption-solubility in relation to cGIC (Fuji IX). The XRD diffractogram indicated the presence of peaks for ZrO₂, SiO₂, and HA. The fracture toughness of GIC 5%nanoZrO₂-SiO₂-HA was statistically higher than that of other percentages of GIC nanoZrO₂-SiO₂-HA and cGIC. The highest values recorded were fracture toughness (1.35 ± 0.15 MPa.m²/2), leading to an increase of ~57%, as compared to cGIC. Overall, the color change (ΔE) values for GIC 5% nanoZr-Si-HA group were lower than those of cGIC over a one-month period and were between slight and perceptible. In addition, GIC 5%nanoZrO₂-SiO₂-HA recorded lower sorption values (23.64 ± 2.3 μgmm⁻³) as compared to cGIC (36.28 ± 2.6 μgmm⁻³) and higher solubility (66.46 ± 2.4 μgmm⁻³) as compared to cGIC (56.76 ± 1.6 μgmm⁻³). The addition of nanoZrO₂-SiO₂-HA to cGIC significantly enhanced its physico-mechanical properties. Based on the results of our study, GIC nanoZrO₂-SiO₂-HA has the potential to be suggested as a restorative dental material with diverse applications ranging from cavity restoration, core build-up, and as a luting material.

1. Introduction

A decline in the use of traditional silver amalgam restorations due to the fear of mercury toxicity and tooth and gingival discoloration has led to increased interest in tooth-colored restorative materials such as GIC and composite resins. Glass ionomer cements were first introduced to dentistry in the late 1960s and have proven to be useful in restorative dentistry. Glass ionomers as a system which is polyelectrolytic and aqueous are easy to manipulate, bond to tooth at an ionic
level, and exhibit fluoride (F) release and recharge, a low coefficient of thermal expansion, and decent aesthetics [1]. They are also biocompatible with pulp, gingival, and bone tissues. However, in the clinical environment, their use has become limited owing to inferior mechanical properties such as low flexural strength and fracture toughness (FT) [2–5]. In addition, a relatively high opacity, moisture susceptibility during early setting phase makes these materials less desirable [6–9]. Therefore, GICs have become restricted to restoring low stress-bearing areas such as proximal and axial wall defects [10].

In order to overcome the drawbacks of GIC, additions to the glass powder such as metallic oxides, strontium, and barium were attempted but these did not have a significant effect on the mechanical properties of GICs since they lacked the ability to increase the cross-linking within the glass matrix [11–13]. Recent research has proven that incorporation of nanoceramics such as hydroxyapatite (HA), silica (SiO₂), and zirconia (ZrO₂) produced via various soft chemistry processes capable of creating nanoscale particles has the potential to improve the properties of GICs [14–17].

Recently at the biomaterials lab at our dental school, a novel nanoZrO₂-SiO₂-HA composite was synthesized by one-pot synthesis and incorporated into conventional GIC (cGIC). The effect induced by the phenomenon of adding nanoZrO₂-SiO₂-HA to the cGIC on its physomechanical properties was analyzed. The addition of nanoZrO₂-SiO₂-HA produced surprising improvements in the compressive strength, flexural strength, and F release of cGIC [18–20]. FTIR characterization of the GIC nanoZrO₂-SiO₂-HA revealed that there was chemical interaction between the polymeric phase of GIC and the nanopowder [19]. However, concerns regarding the FT, color stability (CS), and sorption-solubility of the nanoZrO₂-SiO₂-HA when added to GIC need to be addressed. Therefore, the aim of this study was to evaluate the FT, CS, and the sorp-sol of the GIC nanoZrO₂-SiO₂-HA hybrid material.

### 2. Methods

Fuji IX Universal (GC Corp., Japan) was selected as the control material for our study as it is a widely used cGIC in dentistry. Fuji IX has also been recommended as the material of choice for atraumatic restorative treatment (ART) by the World Health Organization (WHO). For manipulation and ease, it is dispensed in the form of an ionomeric powder and liquid polyacid. The various other chemicals and reagents used for the synthesis of nanoZrO₂-SiO₂-HA were of high purity and analytical grade, which were purchased commercially. First, the nano HA was synthesized using the sol-gel technique described by Rahman et al. (2017) [21]. Calcium hydroxide (>98%) (Merck Serono Pvt. Australia) and phosphoric acid (>99%) (Sigma-Aldrich Co. LLC, USA) was the primary sources for calcium and phosphorus. A quantity of 7.408 g of calcium hydroxide dissolved into 100 ml of distilled water, 4.104 ml of phosphoric acid, and 5 ml of TEOS (Merck Serono Pvt. Australia) and 25% ZrO₂ (US Research Nanomaterials, USA) were used to make the sol. The white viscous sol was washed with copious absolute ethanol (HmbG Chemicals, Germany) and was conditioned for 1 h in a -80°C freezer and finally freeze-dried under vacuum for 24 h. The resultant powder was manually ground for 10 mins using a mortar and immediately calcined at 600°C for 1 h in a furnace oven. The quantity of nano ZrO₂ and nano SiO₂-HA in the nanopowder composite are presented in Table 1.

#### 2.1. XRD Characterization. 

The qualitative analysis of the synthesized nanopowder was carried out XRD (D2 PHASER, Bruker Technologies, USA). The nanopowder was placed on the double-sided carbon-based tape and placed inside the XRD machine. The analysis was performed at a rate of 0.02 min⁻¹. CuKα radiation was used with a current of 10 mA operating at 30 kV.

#### 2.2. Fracture Toughness Evaluation

Fracture toughness was determined according to the method outlined in ASTM specification E-399-90 for single-edge V-notch beam (SEVNB) samples loaded in transverse bending. Fifty knife-edge notch samples (n = 10/group) with dimensions of 25 mm × 2.5 mm × 5 mm were prepared in a split metal mold. The nanoZrO₂-SiO₂-HA powder was added at various percentages (3%, 5%, 7%, and 9%) by volume, into the cGIC to prepare a total of four experimental groups. The powder of GIC nanoZrO₂-SiO₂-HA together with liquid was then mixed using spatulation technique on the mixing pad with an agate spatula for 30 sec in a clockwise direction. The cement mix was condensed into the mold that was then pressed between two polyester strip and glass plates under load for 10 min. The beam-shaped samples were carefully removed from and stored at 37°C in 100% humidity for 50 min then in distilled water for 23 h. A notch with 0.5 mm width and 2.5 mm depth was prepared using a low-speed diamond band saw (Exakt 300, Exakt Tech. Inc., USA). The notch tip was refined and sharpened with the help of a razor blade in a gentle back and forth motion [22].

A three-point bending test was done in a universal testing machine (AG-X plus 20 KN, Shimadzu, Japan) at a crosshead speed of 0.5 mm/min. The moment a sample cracks was determined according to the method outlined in ASTM specification E-97-95 and the control GIC. The analysis was performed at a rate of 0.02 min⁻¹. CuKα radiation was used with a current of 10 mA operating at 30 kV.

### Table 1: Powder composition of nanoZrO₂-SiO₂-HA.

| Composite          | Mass of HA (g) | Mass of SiO₂ (g) | Mass of ZrO₂ (g) | Powder composition |
|-------------------|----------------|------------------|------------------|--------------------|
| NanoZrO₂-SiO₂-HA | 10.04          | 1.356            | 3.79             | 66.75% HA, 8.25% SiO₂, 25% ZrO₂ |

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Fracture toughness, \(K_{1c}\) (MPa-m\(^{1/2}\)), was calculated from the following equation:

\[
K_{1c} = \frac{(P_q S)}{(BW^{3/2})} \cdot F\left(\frac{a}{W}\right),
\]

where \(P_q\) is the peak load (kN), \(S\) is the span (cm), \(B\) is the sample thickness (cm), \(W\) is the sample width (cm), and \(a\) is the crack length (cm). \(F(a/W)\) is a function of \(a/W\) and is calculated as:

\[
F(a/W) = 3(a/W)^{1/2} \times 1:99 - (a/W) (1 - a/W) (1 - a/W) \times (2.25 - 3.93 a/W + 2.7a^2/W^2/2 (1 + 2 a/W)) 1 - a/W)^{3/2}.
\]

2.3. Color Stability Evaluation. The results of FT found that GIC 5% nanoZrO\(_2\)-SiO\(_2\)-HA exhibited superior properties compared to cGIC and other groups. Therefore, from here forth for all the other testing GIC 5% nanoZrO\(_2\)-SiO\(_2\)-HA was evaluated. A total of 20 samples (\(n = 10/\text{group}\)) were prepared, measuring 5 mm in diameter \(\times\) 2 mm in thickness. The powder and liquid were mixed and loaded in a PTFE split mold. The mold was then covered with polyester strips and pressed with a glass plate. After 15 min, samples were removed from the mold, and a baseline color measurement was taken with a portable spectrophotometer with a measurement range of 400–700 nm (VITA Easyshade\textsuperscript{®} Advance 4.0, VITA Zahnfabrik, Germany). During the test, period samples were stored at 37 \(\pm\) 1 °C and 100% relative humidity in airtight containers. The CIE (Commission internationale de l’éclairage) \(L^∗, a^∗, b^∗\) values of the GIC 5% nanoZrO\(_2\)-SiO\(_2\)-HA experimental group were compared to the cGIC group to evaluate color change from baseline to the final measurement.

The CIELAB coordinates of each sample were measured at the following time intervals: baseline, day one, day seven, day 14, and day 28. This time duration was selected in order to detect any apparent change in the color of the samples. The spectrophotometer was calibrated before each measurement session using the white calibration tile supplied by the manufacturer. Three readings were taken at the center of each sample with a standardized white background below. The samples were not allowed to dehydrate and were kept moist throughout the experiment. They were blotted dry just prior to measurement. The colorimetric values were calculated using the equation below, where \(\Delta E\) is the color change, \(\Delta L^∗\) is the change in value, and \(\Delta a^∗\) and \(\Delta b^∗\) represent the changes in the chromatic coordinates.

\[
\Delta E = [(\Delta L^*)^2 + (\Delta a^*)^2 + (\Delta b^*)^2]^{1/2}.
\]

To emphasize and provide a reference guideline, the results of color changes (\(\Delta E\)) values were presented along with National Bureau of Standards (NBS) values by applying the following formula: NBS = \(\Delta E \times 0.92\).

2.4. Sorption-Solubility Evaluation. Sorption-solubility samples were prepared using PTFE molds with an inner dimension of 10 \(\times\) 2 mm. Twenty disc-shaped samples were prepared as previously described in color stability sample preparation. Samples were stored in a silica gel desiccator set at 37 \(\pm\) 1 °C for 22 h. Following which, samples were transferred to a second desiccator at 25 \(\pm\) 1 °C for 2 h. The samples were then weighed in a digital analytical balance machine with a resolution of 0.1 mg (Mettler Toledo\textsuperscript{™}, Fisher Scientific\textsuperscript{™}, USA) every single day at the same hour of the day, and this cycle was repeated until a constant mass was acquired (\(m_1\)). The mass was considered constant if it showed mass variations of up to 0.1 mg from the previous day. After recording \(m_1\), the samples were stored in artificial saliva for 7 days at 37 \(\pm\) 1 °C after which the samples were removed, blot dried with absorbent paper, and weighed for the second time (\(m_2\)). Following this, the samples were stored in the desiccators as detailed in the storage protocol used for \(m_1\), until a constant mass was achieved (\(m_3\)). The volume (\(V\)) of each sample was calculated in mm\(^3\). Water sorption (\(W_{sp}\)) and solubility (\(W_{sl}\)) values for each sample were calculated using the following equations given below, where \(m\) is mass and \(V\) is sample volume and the mean of sorption-solubility was recorded in \(\mu\)gmm\(^{-3}\).

\[
W_{sp} = \frac{m_2 - m_3}{V},
\]

\[
W_{sl} = \frac{m_1 - m_3}{V}.
\]

2.5. Statistical Analysis. For FT, the data was statistically analyzed using IBM SPSS version 23 (IBM Corp., USA). One-way analysis of variance (ANOVA) coupled with a post hoc Tukey HSD multiple range test was used to determine a significant difference (\(\alpha \leq 0.05\)). Whereas for CS repeated measure analysis of variance (ANOVA), with a Bonferroni correction was employed and for sorption solubility, independent sample \(t\)-test (two-tailed) was used.

3. Results

3.1. XRD Characterization. The diffraction patterns indicated the presence of peaks of ZrO\(_2\), SiO\(_2\), and HA (Figure 1). The first peak at \(~23^\circ\) belongs to 120 plane of SiO\(_2\) and another...
peak at ~25° corresponds to 002 plane of HA and 011 plane of SiO₂. Similarly, another peak at ~28° also represents 102 plane of HA and 111 plane of SiO₂. These findings are in accordance to those of previously published literature [14, 23]. The XRD displayed a very strong peak at ~32° that corresponded to the 112 plane of HA; 012 plane of SiO₂ and 011 plane of ZrO₂. Next, a shoulder peak at ~34° was due to the 300 plane of HA, and 002 plane of ZrO₂ indicated the presence of HA that was not as predominant as pure HA crystal and could be attributed to the silicon doping effect. Other smaller peaks at ~40°, 46, 49, and 55 correspond to HA (212), SiO₂ (113), ZrO₂ (020), and HA (312), respectively. Peaks through ~59–60° are those of 121 planes of ZrO₂ and finally peak at ~65° represent 104 and 132 plane of HA and SiO₂, respectively. These findings are similar to the characterization studies published previously [14, 23, 24]. The particle size was calculated by taking 32° peak as the reference peak and full with half maxima (FWHM) as 0.4 using the Scherrer’s equation (Particle size = \( \frac{\lambda \cdot \theta}{\beta \cdot \cos \theta} \)), where \( \lambda \) is the wavelength of Cuka = 0.15148 mm, \( \beta \) = 0.4, \( 2\theta = 32° \), and \( \theta = 16° \) converted in radians and was found to be 21.62 mm.

The phase purity and information of various chemical species have been characterized by XRD, and nanocrystalline nature has been ascertained by XRD. All of the peaks in XRD patterns have a good match with the standard of HA, ZrO₂, and SiO₂ phase in terms of position of the lines. A decrease in the crystallinity of HA at ~34° in the nanopowder composite indicates the presence of amorphous SiO₂. The diffraction peaks centred at ~32° (011) and ~34° (002) are characteristics of the tetragonal ZrO₂. These findings suggest that a nanoZrO₂-SiO₂-HA composite was synthesized by the one-pot sol-gel method.

3.2. Fracture Toughness. The results of the FT test after 1-day immersion in distilled water for cGIC (Fuji IX) and four GIC nanoZrO₂-SiO₂-HA experimental groups are shown in Table 2. The FT of cGIC was the lowest recorded among the groups (Figure 2) with a mean \( K_{IC} \) value of 0.78 MPa.m\(^{1/2} \) (±0.20). The maximum recorded \( K_{IC} \) value of 1.65 MPa.m\(^{1/2} \) was for GIC 5% nanoZrO₂-SiO₂-HA with a mean \( K_{IC} \) value of 1.35 MPa.m\(^{1/2} \) (±0.15). There was a significant statistical difference between FT values of GIC 5% nanoZrO₂-SiO₂-HA and all the other groups except GIC 3% nanoZrO₂-SiO₂-HA with (p = 0.061).

3.3. Color Stability. Results are showed in Tables 3 and 4 which reflect the color change (ΔE) between the various time intervals and between day 1 (baseline) and the different time intervals, respectively. There was a statistically significant difference between the day 1 to day 7 and day 14 to day 28 ΔE values (Table 3) for cGIC (ΔE₁ = 2.40 and ΔE₇ = 2.72) and GIC 5% nanoZrO₂-SiO₂-HA (ΔE₁ = 3.26 and ΔE₇ = 3.32). However, ΔE₂ and ΔE₆ for GIC 5% nanoZrO₂-SiO₂-HA are much lower as compared to the cGIC group (Figure 3) which implies that the color of GIC 5% nanoZrO₂-SiO₂-HA became more stable over time and did not change. Table 4 shows a statistically significant difference between the day 1 and day 28 ΔE values for cGIC (ΔE₆ = 3.56) and GIC 5% nanoZrO₂-SiO₂-HA (ΔE₆ = 2.75) which is also depicted graphically in Figure 4. Also, the NBS unit for the cGIC group corresponding to ΔE₆ was 3.2 indicative of appreciable color change. Whereas the NBS units for GIC 5% nanoZrO₂-SiO₂-HA were between 2.0 and 3.0 and were indicative of only perceptible color change.

3.4. Sorption- Solubility. GIC 5% nanoZrO₂-SiO₂-HA recorded higher values for solubility but lesser values for sorption when compared with cGIC (Figure 5). Results reported for solubility value of GIC 5% nanoZrO₂-SiO₂-HA (66.46 ± 2.4 μggmm\(^{-3} \)) was higher than cGIC (56.76 ± 1.6 μggmm\(^{-3} \)) which could explain the higher
initial F− burst observed in our previous study [18] and also by other researchers [25], and it was found to be statistically significant (Table 5). Whereas the sorption of GIC 5% nanoZrO2-SiO2-HA (23.64 ± 2.3 μg mm−3) was significantly lower than that of cGIC (36.28 ± 2.6 μg mm−3) which is an appreciable attribute as higher sorption can adversely affect the mechanical properties and color stability of the material.

### 4. Discussion

The most common causes of failure of GICs were related to fractures and wear out. Several studies have inferred that FT measurement should be considered the single most useful predictor of a material’s clinical performance over other parameters presently used for evaluation. Fracture toughness is the instantaneous stress condition (KIC value) at the initiation of the crack propagation and KIC (plane–strain fracture toughness)
toughness) in particular is an essential parameter that represents mode I type of fracture opening [26–28]. There was a partial linear correlation between the FT values and the % volume addition of nanoZrO₂-SiO₂-HA to the GIC up to 5% following which any further addition of nanoZrO₂-SiO₂-HA to the GIC led to a FT decrease. These observations are in accordance with the findings of a couple of other studies in which the researchers evaluated the effect of glass fibres on the FT of GIC [29, 30]. This could be due to overcrowding of filler particles, which may interfere with the polysalt bridge formation within the GIC. In general, all the GIC nanoZrO₂-SiO₂-HA experimental groups had higher FT values than the cGIC group. This is probably due to the toughening effect of ZrO₂ and the additive effect of HA. The homogeneous incorporation of nanoparticles in the glass component further reinforces the structural integrity of the GIC for high load tolerance and lasting durability [31–33].

Color stability is critical to the long-term success of any aesthetic restoration. The highest recorded ΔΕ was observed between day 1 and day 7 time interval (ΔΕ₁ = 3.26) for GIC 5% nanoZrO₂-SiO₂-HA. This finding agrees with another study, where the authors reported similar observations [34]. However, after the ΔΕ₁ time interval, ΔΕ values for GIC 5% nanoZrO₂-SiO₂-HA were <1.40 and remained stable for the duration of the study. It can be hypothesized that the nanoZrO₂-SiO₂-HA particles fill the void between the glass particles, improving the packing density and prevent the possibility of phase separation during setting of the material, thereby improving the CS of cGIC. Since a ΔΕ value of up to 3.3 is considered to be clinically acceptable in dentistry, it can be concluded that the color of GIC 5% nanoZrO₂-SiO₂-HA was stable [35, 36]. Overall, the ΔΕ values for GIC 5% nanoZrO₂-SiO₂-HA group were lower than those of the cGIC group. The evaluation of visual perception of color change determination based on the NBS unit system was also done, which dictates that values of 0.5 to 1.5 are considered slight, values between 1.5 and 3 are perceptible, and values >3 are interpreted as appreciable color change [37, 38]. The color change between various time intervals shows that the NBS units for GIC 5% nanoZrO₂-SiO₂-HA group were between 1.0 and <3.0 and generally were lower than those of the cGIC group which were between 2.0 and 3.5. Therefore, according to NBS system, the color change for GIC 5% nanoZrO₂-SiO₂-HA was between slight and perceptible.

In the current study, water sorption values for GIC 5% nanoZrO₂-SiO₂-HA (23.64 ± 2.3 μgmm⁻³) were significantly lower than cGIC (36.28 ± 2.6 μgmm⁻³). This is an encouraging finding as sorbed water acts as a plasticizer and can reduce the mechanical properties of GIC. Also, increased water sorption usually decreases the color stability of GIC as water-soluble stains can enter the glass matrix [25, 39]. Therefore, it can be assumed that the GIC 5% nanoZrO₂-SiO₂-HA will continue to display improved mechanical strength and color stability in vivo. The low water sorption could be the result of the nanoZrO₂, SiO₂, and HA particles filling the spaces between the micron-sized glass particles of cGIC and optimum filler content resulting in a dense network structure. However, an increase in solubility was demonstrated by GIC 5% nanoZrO₂-SiO₂-HA as compared to cGIC and could be due to an improved F ion release [18]. This is because the F releasing capacity of restorative materials is related to their ability to support diffusion without allowing excessive water sorption.

5. Conclusion

Within the limitations of this study, certain conclusions can be agreed upon and they are as follows: (a) XRD characterization studies revealed that nanoZrO₂-SiO₂-HA was properly synthesized and homogenously incorporated into the cGIC, (b) The GIC 5%nanoZrO₂-SiO₂-HA exhibited significantly higher fracture toughness when compared to cGIC and other experimental groups, and (c) the GIC 5%nanoZrO₂-SiO₂-HA exhibited a statistically significant improvement in color stability over cGIC. Also, GIC 5% nanoZrO₂-SiO₂-HA exhibited a significantly lower water sorption but higher solubility than cGIC. Based on the above findings, the GIC nanoZrO₂-SiO₂-HA can be recommended for wider application such as in aesthetic areas for restoring class V cavities, for restoring posterior teeth in stress-bearing areas, as a core build-up material and as an improved substitute for atraumatic restorative therapy.

Data Availability

The data used to support the findings of this study are available from the corresponding author upon request.

Conflicts of Interest

The authors disclose that there is no conflict of interest regarding the publication of this manuscript.

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