Research Article

PET Imaging of Crossed Cerebellar Diaschisis after Long-Term Cerebral Ischemia in Rats

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Crossed cerebellar diaschisis (CCD) is a decrease of regional blood flow and metabolism in the cerebellar hemisphere contralateral to the affected brain hemisphere as a common consequence of a supratentorial cerebral malfunction [1–3]. Previous studies have suggested that the remote deactivation of cerebellar neurons can be promoted as a result of the interruption of excitatory impulses by the corticopontocerebellar tract [4]. CCD has been reported in several diseases affecting the brain such as cerebral gliomas [5], epilepsy [6], intracerebral hemorrhage [7, 8], and stroke [3, 9–11], among others. In the latter, CCD has been detected at the acute, subacute, and chronic phases. As a result, CCD has been postulated as a prognostic indicator of neurological outcome after cerebrovascular diseases [12, 13]. Nevertheless, other studies have evidenced controversies regarding the correlation of CCD to the location and size of the brain injury and to the clinical severity [14, 15]. In view of these controversial results, the use of in vivo imaging techniques acquires a relevant role in the investigation of the precise role of CCD on stroke pathophysiology. CCD in human supratentorial brain infarction has been detected with positron emission tomography (PET) imaging with 2-deoxy-2-[18F]fluoro-D-glucose ([18F]FDG). Imaging studies were combined with neurological evaluation to assess functional recovery. In the ischemic territory, imaging studies showed a significant decrease in glucose metabolism followed by a progressive recovery later on. Conversely, the cerebellum showed a contralateral hypometabolism from days 7 to 14 after reperfusion. Neurological behavior showed major impaired outcome at day 1 after ischemia followed by a significant recovery of the sensorimotor function from days 7 to 28 after experimental stroke. Taken together, these results suggest that the degree of CCD after cerebral ischemia might be predictive of neurological recovery.

1. Introduction

Crossed cerebellar diaschisis (CCD) is a decrease of regional blood flow and glucose metabolism in the cerebellar hemisphere contralateral to the affected brain hemisphere as a common consequence of a supratentorial cerebral malfunction [1–3]. Previous studies have suggested that the remote deactivation of cerebellar neurons can be promoted as a result of the interruption of excitatory impulses by the corticopontocerebellar tract [4]. CCD has been reported in several diseases affecting the brain such as cerebral gliomas [5], epilepsy [6], intracerebral hemorrhage [7, 8], and stroke [3, 9–11], among others. In the latter, CCD has been detected at the acute, subacute, and chronic phases. As a result, CCD has been postulated as a prognostic indicator of neurological outcome after cerebrovascular diseases [12, 13]. Nevertheless, other studies have evidenced controversies regarding the correlation of CCD to the location and size of the brain injury and to the clinical severity [14, 15]. In view of these controversial results, the use of in vivo imaging techniques acquires a relevant role in the investigation of the precise role of CCD on stroke pathophysiology. CCD in human supratentorial brain infarction has been detected with positron emission tomography (PET) and single photon emission computed tomography (SPECT) [13, 14, 16–19]. Alternatively to nuclear imaging techniques, arterial spin-labeling (ASL) has also proven efficient for the evaluation of CCD after hyperacute and acute ischemic stroke [9, 20]. Unexpectedly, although CCD has been detected in patients with stroke, the in vivo imaging evaluation of this...
phenomenon in rodent models of cerebral ischemia has been never evaluated so far. Here, we report the unprecedented investigation of CCD after long-term cerebral ischemia in a rat model of experimental stroke using PET with 2-deoxy-2-[18F]fluoro-D-glucose ([18F]FDG). Glucose metabolic changes in the ischemic brain (cerebrum, cortex, and striatum) were also investigated, and the results were correlated to the neurological outcome evolution over time. Our studies show contralateral cerebellar hypometabolism at the acute and subacute phases of ischemia and a correlation between the presence of CCD and the improvement of neurological outcome. Hence, these results reported here will provide novel information on the detection of the CCD in experimental stroke that might ultimately contribute to a better comprehension of the role of this phenomenon during stroke evolution.

2. Materials and Methods

2.1. Cerebral Ischemia. 9-week-old male Sprague-Dawley rats (n = 6; 295 ± 6.2 g body weight; Janvier, France) were used for imaging studies. Rats were anaesthetized with 2.5% isoflurane in 100% O2 and transient focal ischemia was produced by a 2-hour intraluminal occlusion of the middle cerebral artery (MCAO) followed by reperfusion as described previously [21]. Six rats were repeatedly scanned before reperfusion (day 0) and at 1, 3, 7, 14, 21, and 28 days after ischemic onset to evaluate glucose metabolism by PET.

2.2. Magnetic Resonance Imaging. T2-weighted (T2W) MRI scans were performed at days 1 (to measure the size of the infarction; n = 6), 3, 7, 14, 21, and 28 after MCAO (to coregister PET signal data; n = 1 per time point). Before the scans, anesthesia was induced with 4% isoflurane and maintained by 2–2.5% of isoflurane and maintained by 2–2.5% of isoflurane in 100% O2. The tail vein was catheterized with a 24-gauge catheter for intravenous administration of the radiotracer. For longitudinal assessment of glucose metabolism with [18F]FDG, animals were scanned before and during the following month after ischemia. The radioactivity (~10 MBq) was injected and after an uptake period of 30 minutes, the animals were reanaesthetized and placed on the PET for a brain static acquisition in the 400–700 keV energetic window, with a total acquisition time of 30 minutes as described elsewhere [23]. After each PET scan, CT acquisitions were also performed (140 μA intensity, 40 kV voltage), to provide anatomical information of each animal as well as the attenuation map for the later PET image reconstruction. Static acquisitions were reconstructed (decay and CT-based attenuation corrected) with filtered back projection (FBP) using a ramp filter with a cut-off frequency of 0.5 mm⁻¹.

2.3. Magnetic Resonance Imaging Image Analysis. MRI (T2W) images were acquired at 1 day after ischemia were used to calculate the lesion volume. Regions of interest (ROIs) were manually defined using the open source software 3D Slicer image analysis software (Version 4.8 http://www.slicer.org) for each rat on the region of increased signal in the ipsilateral hemisphere. The total lesion volume was calculated by summing the area of the infarcted regions of all slices affected by the lesion.

2.4. Radiochemistry, Positron Emission Tomography Scans, and Data Acquisition. [18F]-2-fluoro-2-deoxy-D-glucose ([18F]FDG) was produced as described earlier [22] and provided by IBA Molecular Spain (San Sebastian, Spain). PET scans were performed using a General Electric eXplore Vista CT camera (GE Healthcare). Scans were performed in rats anaesthetized with 4% isoflurane and maintained by 2–2.5% of isoflurane in 100% O2. The tail vein was catheterized with a 24-gauge catheter for intravenous administration of the radiotracer. For longitudinal assessment of glucose metabolism with [18F]FDG, animals were scanned before and during the following month after ischemia. The radioactivity (~10 MBq) was injected and after an uptake period of 30 minutes, the animals were reanaesthetized and placed on the PET for a brain static acquisition in the 400–700 keV energetic window, with a total acquisition time of 30 minutes as described elsewhere [23]. After each PET scan, CT acquisitions were also performed (140 μA intensity, 40 kV voltage), to provide anatomical information of each animal as well as the attenuation map for the later PET image reconstruction. Static acquisitions were reconstructed (decay and CT-based attenuation corrected) with filtered back projection (FBP) using a ramp filter with a cut-off frequency of 0.5 mm⁻¹.

2.5. Positron Emission Tomography Image Analysis. PET imaging analysis was performed according to our previously published procedure [24]. PET images were analyzed using PMOD image analysis software (PMOD Technologies Ltd, Zürich, Switzerland). To verify the anatomical location of the signal, PET images were coregistered to the anatomical data of a MRI rat brain template. Two type of volumes of interest (VOIs) were established as follows: (i) A first set of VOIs was defined to study the whole brain and cerebellum [18F]FDG PET signal. Whole brain and cerebellum VOIs were manually drawn in both the entire ipsilateral and contralateral hemispheres on slices of a MRI (T2-W) rat brain template from the PMOD software. (ii) A second set of VOIs was automatically generated in the cortex and the striatum by using the regions proposed by the PMOD rat brain template, to study the evolution of [18F]FDG PET signal in these specific regions in both the ipsilateral and contralateral cerebral hemispheres. PET signal uptake was averaged in each ROI and expressed as percentage of injected dose per cubic centimetre (%ID/cc), and the hemispheres ratios were considered.

2.6. Neurological Assessment. The assessment of neurological outcome induced by cerebral ischemia was based on a previously reported 9-neuroscore test [25]. Before imaging evaluations, four consecutive tests were performed at days 1 and 7 after ischemia in treated and control rats as follows: (a) spontaneous activity (moving and exploring = 0, moving without exploring = 1, no moving = 2); (b) left drifting
during displacement (none = 0, drifting only when elevated by the tail and pushed or pulled = 1, spontaneous drifting = 2, circling without displacement or spinning = 3), (c) parachute reflex (symmetrical = 0, asymmetrical = 1, contralateral forelimb retracted = 2), and (d) resistance to left forepaw stretching (stretching not allowed = 0, stretching allowed after some attempts = 1, no resistance = 2). Total score could range from 0 (normal) to a 9 (highest handicap) point-scale.

2.7. Statistical Analyses. PET imaging comparisons within ischemic group were made with one-way ANOVA followed by Tukey’s multiple-comparison tests for post hoc analysis. Behavioral data have been compared with Mann–Whitney U tests. The level of significance was regularly set at \( P < 0.05 \). Statistical analyses were performed with GraphPad Prism version 6 software.

3. Results

The cerebral glucose metabolism was explored by PET imaging during the first month after transient focal ischemia in rats. All the images were quantified in standard units, i.e., %ID/cc of \([^{18}F]FDG\). The images with normalized color scale illustrate the evolution of the PET signals at control (day 0) and at 1, 3, 7, 14, 21, and 28 days after ischemia onset (Figure 1). The extent of brain damage after cerebral ischemia was assessed using \( T_2 \)W MRI at 1 day after reperfusion. Hyperintensities of \( T_2 \)W images showed similar infarct extents as well as locations affected. All ischemic rats subjected to nuclear studies showed cortical and striatal MRI alterations (mean \( \pm \) s.d.: 296.24 \( \pm \) 48.3 mm\(^3\), \( n = 6 \)).

3.1. \([^{18}F]FDG\) after Cerebral Ischemia. The time course of the cerebral glucose metabolism was evaluated with \([^{18}F]FDG\) in both the ipsilateral and contralateral cortices, striatum, and whole brain at control and 1, 3, 7, 14, 21, and 28 days after MCAO (Figure 1, \( n = 6 \)). The different regions evaluated showed similar metabolic evolution after long-term focal cerebral ischemia. In the whole brain (cerebrum), the ratio of the \([^{18}F]FDG\) signal uptake in the ipsilateral to contralateral hemispheres showed a general metabolic decrease in the ipsilateral hemisphere after cerebral ischemia in relation to control (day 0) values (\( p < 0.001 \), Figure 1(b)). At day 1, the \([^{18}F]FDG\) signal ratio showed the lowest values in comparison to day 0 (control) followed by a progressive increase from day 3 to days 7–14 after ischemia in comparison to day 1 (\( p < 0.01 \); \( p < 0.001 \), Figure 1(b)). Subsequently, the PET signal ratio displayed a slight decrease from days 21 to 28 after ischemia onset (\( p < 0.01 \), Figure 1(b)). The cerebral cortex showed a significant reduction of the \([^{18}F]FDG\) ratio from 1 at day 0 to 0.5 at day 1 after reperfusion followed by a recovery to circa 0.7 at days 7 and 14 and a subsequent decrease later on (days 21–28) (\( p < 0.05 \); \( p < 0.01 \); \( p < 0.001 \), with respect to control and day 1, Figure 1(c)). In addition, the striatum showed similar \([^{18}F]FDG\) PET signal values over the first month after cerebral ischemia than that observed in the whole brain and cerebral cortex (\( p < 0.05 \); \( p < 0.01 \); \( p < 0.001 \), with respect to control and day 1, Figure 1(d)).

3.2. Crossed Cerebellar Diaschisis after Ischemia. The time course of the glucose metabolism in the cerebellum was evaluated with \([^{18}F]FDG\) at the acute, subacute, and chronic stages after MCAO (Figure 2, \( n = 6 \)). In the cerebellum, the ratio of the contralateral to ipsilateral hemispheres showed a progressive glucose metabolism decrease from control (day 0) to day 3 followed by a significant decrease at days 7 and 14 in comparison to day 0 and day 1 after cerebral ischemia. Therefore, these results evidence the existence of CCD after cerebral ischemia in rats (\( p < 0.05 \); \( p < 0.01 \), Figure 2(b)). Subsequently, the \([^{18}F]FDG\) signal ratios displayed a recovery to control values at days 21 and 28 after MCAO. The time course of the neurologic score after cerebral ischemia showed the major neurologic impairment at day 1 after MCAO in relation to control rats followed by a progressive significant improvement from days 7 to 28 after ischemia (\( p < 0.05 \); \( p < 0.01 \); \( p < 0.001 \), with respect to control and day 1, Figure 2(c)).

4. Discussion

Since Baron and collaborators coined the term CCD in the 1980s to describe the disturbance of the cerebellum distant but linked to an ischemic region of the brain, the pathophysiology underlying this phenomenon has been still plenty of controversy [3, 10]. Some clinical studies in stroke have defined diaschisis as a transient and reversible event attributed to a functional neuronal deafferentation. However, others have described CCD as a persistent process that leads to neurodegeneration [18, 26–28]. Likewise, CCD has been extensively diagnosed clinically with neuroimaging modalities in patients at different stages after stroke [9, 11, 13, 29–31]. Despite this, CCD has remained poorly characterized in animal models of stroke. Because of this, we have assessed for the first time the in vivo imaging of CCD using PET with \([^{18}F]FDG\) imaging in combination to neurofunctional evaluation after cerebral ischemia in rats.

4.1. \([^{18}F]FDG\)-PET Imaging after Cerebral Ischemia. Contralateral cerebellar hypometabolism (CCH) is a well-established remote functional effect related to CCD that might be promoted by the uncoupling of the oxygen consumption and glucose utilization caused by neuronal deafferentation [32]. Moreover, it is known that astrocytes respond to neuronal deafferentation and a recent report indicates that \([^{18}F]FDG\) signal is sensitive to astrocyte metabolism suggesting the potential role of astrocytes on CCH [33, 34]. Contralateral cerebellar hypometabolism has been observed clinically with \([^{18}F]FDG\)-PET imaging after stroke; however, the correlation to the clinical significance is still under debate [12]. Therefore, the preclinical characterization of the CCH in animal models of cerebral ischemia with \([^{18}F]FDG\) might provide novel perspectives to the understanding of CCD after stroke. In the present study, we have assessed the characterization of the CCH during the
first month following cerebral ischemia in rats by using \(^{18}\text{F}\) FDG. After experimental stroke, rats showed a decreased \(^{18}\text{F}\)FDG uptake in the region of the infarction followed by a progressive recovery during the first week after ischemia onset (Figure 1). In fact, the increase of glucose metabolism at day 7 stands in agreement with the activation of microglial cells and infiltrated leukocytes after cerebral ischemia [24, 35]. Subsequently, \(^{18}\text{F}\)FDG PET showed a progressive decrease of the glucose metabolism from day 14 to 28 due to a (i) reduction of the inflammatory response and (ii) the
reabsorption of the necrotic cerebral tissue [36, 37]. In addition, as a result of the supratentorial ischemic lesion, PET imaging with [18F]FDG displayed a contralateral cerebellar hypometabolism from days 7 to 14 after MCAO that was followed by a recovery to control values during the second and the third week later on (Figure 2). In addition, we have previously demonstrated that [18F]FDG signal did not show any change over one month in both control and SHAM 9-week-old male Sprague-Dawley rats [23]. Therefore, these results evidence the existence of CCD after acute and subacute stages of cerebral ischemia in rats that are reverted at the chronic phase and are in agreement with the reversibility of the CCH in some patients with stroke [12]. Nevertheless, despite only one-third of the patients in the acute phase showed CCD after large anterior circulation vessel occlusion [31, 38], all rats evaluated in this study presented cerebellar diaschisis. Likewise, the ischemic rats included in this study showed a very similar location and size of lesion (296.24 ± 48.3 mm³). However, the extension of the lesion did not show a significant correlation to the CCH observed at days 7 and 14 after MCAO (data not shown). Therefore, these results are in disagreement with those described by Infield and colleagues who defined CCD as the functional phenomenon that correlates with the severity of the ischemic lesion [15]. In the present study, the neurological score showed that the animals presented the worst outcome at the day 1 after ischemia followed by a progressive significant functional improvement from day 7 to onwards. Therefore, the neurological recovery experienced by the ischemic rats run in parallel with the presence of the CCD at the second and third week after cerebral ischemia. Likewise, these findings stand in contrast with the description of cerebellar diaschisis as the phenomenon that can persist despite the recovery of neuronal functionality [15].

In summary, PET imaging with [18F]FDG was carried out to evaluate the CCD after cerebral ischemia in rats. Our studies showed for the first time the contralateral cerebellar hypometabolism at the acute and subacute phases of cerebral ischemia in rats. Besides, the presence of CCD stands in agreement with the improvement of neurological outcome. Therefore, these results provide valuable knowledge regarding the role of CCD after experimental stroke and suggest that the degree of cerebellar diaschisis might be predictive of neurological recovery in rats.

Figure 2: PET images of [18F]FDG at day 0 (control), day 7, day 14 and day 28 after MCAO (a). Time course of the progression of the [18F] FDG PET signal (n = 6) was shown as the ratio of the entire contralateral to ipsilateral cerebellar hemisphere. The upper right panel of the figure shows the selected brain ROIs for the quantification defined on a slice of a MRI (T2W) template (b). Neurologic outcomes before (day 0) and at 1, 3, 7, 14, 21 and 28 days after cerebral ischemia (c). ***p < 0.001 compared to control, #p < 0.05, ##p < 0.01 and ### p < 0.01 compared to day 1.
Data Availability
All data supporting the results can be found at CICbiomaGUNE, San Sebastian, Spain, or from the corresponding author upon request.

Ethical Approval
Animal experimental protocols were approved by the animal ethics committee of CIC biomaGUNE and the local authorities and were conducted in accordance with the ARRIVE guidelines and Directives of the European Union on animal ethics and welfare.

Conflicts of Interest
The authors declare no conflicts of financial interest.

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References
[1] J. C. Baron, M. G. Bousser, D. Comar, and P. Castaigne, “Crossed cerebellar diaschisis in human supratentorial brain infarction,” Transactions of the American Neurolological Association, vol. 105, pp. 459–461, 1981.
[2] J. C. Baron, D. Rougemont, F. Soussaline et al., “Local interrelationships of cerebral oxygen consumption and glucose utilization in normal subjects and in ischemic stroke patients: a positron tomography study,” Journal of Cerebral Blood Flow & Metabolism, vol. 4, no. 2, pp. 140–149, 1984.
[3] W. G. Kunz, W. H. Sommer, C. Hohne et al., “Crossed cerebellar diaschisis in acute ischemic stroke: impact on morphologic and functional outcome,” Journal of Cerebral Blood Flow & Metabolism, vol. 37, no. 11, pp. 3615–3624, 2017.
[4] L. Gold and M. Lauritzen, “Neuronal deactivation explains decreased cerebellar blood flow in response to focal cerebral ischemia or suppressed neocortical function,” Proceedings of the National Academy of Sciences, vol. 99, no. 11, pp. 7699–7704, 2002.
[5] X. Liu, J. Li, Q. Xu et al., “Pathological factors contributing to crossed cerebellar diaschisis in cerebral gliomas: a study combining perfusion, diffusion, and structural MR imaging,” Neuroradiology, vol. 60, no. 6, pp. 643–650, 2018.
[6] M. A. N. Ferilli, V. Brunetti, E. M. Costantini, and G. Della Marca, “Left hemispheric status epilepticus with crossed cerebellar diaschisis,” Journal of Neurology, Neurosurgery & Psychiatry, vol. 89, no. 3, pp. 311–312, 2018.
[7] D. S. Sin, M. H. Kim, S. A. Park, M. C. Joo, and M. S. Kim, “Crossed cerebellar diaschisis: risk factors and correlation to functional recovery in intracerebral hemorrhage,” Annals of Rehabilitation Medicine, vol. 42, no. 1, pp. 8–17, 2018.
[8] L. Yin, S. Cheng, J. Xiao et al., “3D pseudocontinuous arterial spin-labeling perfusion imaging detected crossed cerebellar diaschisis in acute, subacute and chronic intracerebral hemorrhage,” Clinical Imaging, vol. 50, pp. 37–42, 2017.
[9] K. M. Kang, C. H. Sohn, S. H. Choi et al., “Detection of crossed cerebellar diaschisis in hyperacute ischemic stroke using arterial spin-labeled MR imaging,” PLoS One, vol. 12, no. 3, Article ID e0173971, 2017.
[10] W. H. Sommer, C. Bollewein, K. M. Thierfelder et al., “Crossed cerebellar diaschisis in patients with acute middle cerebral artery infarction: occurrence and perfusion characteristics,” Journal of Cerebral Blood Flow & Metabolism, vol. 36, no. 4, pp. 743–754, 2016.
[11] M. K. Strother, C. Buckingham, C. C. Faraco et al., “Crossed cerebellar diaschisis after stroke identified noninvasively with cerebral blood flow-weighted arterial spin labeling MRI,” European Journal of Radiology, vol. 85, no. 1, pp. 136–142, 2016.
[12] C. Serrati, G. Marchal, P. Rioux et al., “Contralateral cerebellar hypometabolism: a predictor for stroke outcome?,” Journal of Neurology, Neurosurgery & Psychiatry, vol. 57, no. 2, pp. 174–179, 1994.
[13] J. Sobesky, A. Thiel, M. Ghaemi et al., “Crossed cerebellar diaschisis in acute human stroke: a PET study of serial changes and response to supratentorial reperfusion,” Journal of Cerebral Blood Flow & Metabolism, vol. 25, no. 12, pp. 1685–1691, 2005.
[14] J. De Reuck, D. Decoo, I. Lemahtieu, K. Strickmанс, P. Goethals, and G. Vamele, “Crossed cerebellar diaschisis after middle cerebral artery infarction,” Clinical Neurology and Neurosurgery, vol. 99, no. 1, pp. 11–16, 1997.
[15] B. Infeld, S. M. Davis, M. Lichtenstein, P. J. Mitchell, and J. L. Hopper, “Crossed cerebellar diaschisis and brain recovery after stroke,” Stroke, vol. 26, no. 1, pp. 90–95, 1995.
[16] K. Kajimoto, N. Oku, Y. Kimura et al., “Crossed cerebellar diaschisis: a positron emission tomography study with L-[methyl-11C]methionine and 2-deoxy-2-[18F]fluoro-D-glucose,” Annals of Nuclear Medicine, vol. 21, no. 2, pp. 109–113, 2007.
[17] S. E. Kim, C. W. Choi, B. W. Yoon et al., “Crossed-cerebellar diaschisis in cerebral infarction: technetium-99m-HMPAO SPECT and MRI,” Journal of Nuclear Medicine, vol. 38, no. 1, pp. 14–19, 1997.
[18] Y. Liu, J. O. Karonen, J. Nuutinen, E. Vanninen, J. T. Kuikka, and R. L. Vanninen, “Crossed cerebellar diaschisis in acute ischemic stroke: a study with serial SPECT and MRI,” Journal of Cerebral Blood Flow & Metabolism, vol. 27, no. 10, pp. 1724–1732, 2007.
[19] P. Pantano, J. C. Baron, Y. Samson, M. G. Bousser, C. Derouesne, and D. Comar, “Crossed cerebellar diaschisis: further studies,” Brain, vol. 109, no. 4, pp. 677–694, 1986.
[20] J. A. Chalela, D. C. Alsop, J. B. Gonzalez-Atavales, J. A. Maldjian, S. E. Kasner, and J. A. Detre, “Magnetic resonance perfusion imaging in acute ischemic stroke using continuous arterial spin labeling,” Stroke, vol. 31, no. 3, pp. 680–687, 2000.
[21] C. Justicia, F. J. Perez-ASENSIO, M. C. Burguete, J. B. Salom, and A. M. Planas, “Administration of transforming growth factor-alpha reduces infarct volume after transient focal cerebral ischemia or suppressed neocortical function,” Proceedings of the National Academy of Sciences, vol. 99, no. 11, pp. 7699–7704, 2002.
[22] K. Hamacher, H. H. Coenen, and G. Stocklin, “Efficient stereospecific synthesis of no-Carrier-added 2-[18F]-fluoro-2-deoxy-D-glucose using aminopolyether supported nucleophilic substitution,” Journal of Nuclear Medicine, vol. 27, no. 2, pp. 235–238, 1986.
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[23] A. Martin, V. Gómez-Vallejo, E. San Sebastián et al., “In vivo imaging of dopaminergic neurotransmission after transient focal ischemia in rats,” Journal of Cerebral Blood Flow & Metabolism, vol. 33, no. 2, pp. 244–252, 2013.

[24] M. Domercq, B. Szczupak, J. Gejo et al., “PET imaging with [(18)F]FSPG evidences the role of system xc(-) on brain inflammation following cerebral ischemia in rats,” Theranostics, vol. 6, no. 11, pp. 1753–1767, 2016.

[25] S. A. Menzies, J. T. Hoff, and A. L. Betz, “Middle cerebral artery occlusion in rats: a neurological and pathological evaluation of a reproducible model,” Neurosurgery, vol. 31, no. 1, pp. 100–106, 1992.

[26] W. H. Kempinsky, “Vascular and neuronal factors in diaschisis with focal cerebral ischemia,” Research publications-Association for Research in Nervous and Mental Disease, vol. 41, pp. 92–115, 1966.

[27] J. Kim, S. K. Lee, J. D. Lee, Y. W. Kim, and D. I. Kim, “Decreased fractional anisotropy of middle cerebellar peduncle in crossed cerebellar diaschisis: diffusion-tensor imaging-positron-emission tomography correlation study,” American Journal of Neuroradiology, vol. 26, no. 9, pp. 2224–2228, 2005.

[28] R. D. Tien and B. C. Ashdown, “Crossed cerebellar diaschisis and crossed cerebellar atrophy: correlation of MR findings, clinical symptoms, and supratentorial diseases in 26 patients,” American Journal of Roentgenology, vol. 158, no. 5, pp. 1155–1159, 1992.

[29] S. Chen, M. Guan, H. J. Lian et al., “Crossed cerebellar diaschisis detected by arterial spin-labeled perfusion magnetic resonance imaging in subacute ischemic stroke,” Journal of Stroke and Cerebrovascular Diseases, vol. 23, no. 9, pp. 2378–2383, 2014.

[30] W. J. Shih, W. S. Huang, and P. P. Milan, “F-18 FDG PET demonstrates crossed cerebellar diaschisis 20 years after stroke,” Clinical Nuclear Medicine, vol. 31, no. 5, pp. 259–261, 2006.

[31] Y. Shinohara, A. Kato, K. Kuya et al., “Perfusion MR imaging using a 3D pulsed continuous arterial spin-labeling method for acute cerebral infarction classified as branch atheromatous disease involving the lenticulostriate artery territory,” American Journal of Neuroradiology, vol. 38, no. 8, pp. 1550–1554, 2017.

[32] H. Yamauchi, H. Fukuyama, Y. Nagahama, S. Nishizawa, and J. Konishi, “Uncoupling of oxygen and glucose metabolism in persistent crossed cerebellar diaschisis,” Stroke, vol. 30, no. 7, pp. 1424–1428, 1999.

[33] H. W. Cheng, T. Jiang, S. A. Brown, G. M. Pasinetti, C. E. Finch, and T. H. Mc Neill, “Response of striatal astrocytes to neuronal deafferentation: an immunocytochemical and structural study,” Neuroscience, vol. 62, no. 2, pp. 425–439, 1994.

[34] E. R. Zimmer, M. J. Parent, D. G. Souza et al., “[18F]FDG PET signal is driven by astroglial glutamate transport,” Nature Neuroscience, vol. 20, no. 3, pp. 393–395, 2017.

[35] A. Martin, B. Szczupak, V. Gomez-Vallejo et al., “In vivo PET imaging of the alpha4beta2 nicotinic acetylcholine receptor as a marker for brain inflammation after cerebral ischemia,” Journal of Neuroscience, vol. 35, no. 15, pp. 5998–6009, 2015.

[36] M. Walberer, S. U. Jantzen, H. Backes et al., “In-vivo detection of inflammation and neurodegeneration in the chronic phase after permanent embolic stroke in rats,” Brain Research, vol. 1581, pp. 80–88, 2014.

[37] Y. W. Jeon, S. H. Kim, J. Y. Lee et al., “Dynamic CT perfusion imaging for the detection of crossed cerebellar diaschisis in acute ischemic stroke,” Korean Journal of Radiology, vol. 13, no. 1, pp. 12–19, 2012.