Assessment of patient based real-time quality control on comparative assays for common clinical analytes

Yide Lu | Fan Yang | Dongmei Wen | Kaifeng Shi | Zhichao Gu | Qiuya Lu | Xuefeng Wang | Danfeng Dong

1Department of Laboratory Medicine, Ruijin Hospital, Shanghai Jiaotong University School of Medicine, Shanghai, China
2Shanghai Senxu Medical Technology Corporation, Shanghai, China
3Faculty of Medical Laboratory Science, Ruijin Hospital, Shanghai Jiaotong University School of Medicine, Shanghai, China

Correspondence
Danfeng Dong and Xuefeng Wang, Department of Laboratory Medicine, Ruijin Hospital, Shanghai Jiaotong University School of Medicine, No 197, Ruijin Er Road, Shanghai, China. Emails: ddf40688@rjh.com.cn; wxf63@shsmu.edu.cn

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Abstract
Background: It is critical for laboratories to conduct multianalyzer comparisons as a part of daily routine work to strengthen the quality management of test systems. Here, we explored the application of patient-based real-time quality controls (PBRTQC)s on comparative assays to monitor the consistency among clinical laboratories.

Methods: The present study included 11 commonly tested analytes that were detected using three analyzers. PBRTQC procedures were set up with exponentially weighted moving average (EWMA) algorithms and evaluated using the AI-MA artificial intelligence platform. Comparative assays were carried out on serum samples, and patient data were collected. Patients were divided into total patient (TP), inpatient (IP), and outpatient (OP) groups.

Results: Optimal PBRTQC protocols were evaluated and selected with appropriate truncation limits and smoothing factors. Generally, similar comparative assay performance was achieved using both the EWMA and median methods. Good consistency between the results from patients’ data and serum samples was obtained, and unacceptable bias was detected for alkaline phosphatase (ALP) and gamma-glutamyl transferase (GGT) when using analyzer C. Categorizing patients’ data and applying specific groups for comparative assays could significantly improve the performance of PBRTQCs. When monitoring the inter- and intraanalyzer stability on a daily basis, EWMA was superior in detecting very small quality-related changes with lower false-positive alarms.

Conclusions: We found that PBRTQCs have the potential to efficiently assess multianalyzer comparability. Laboratories should be aware of population variations concerning both analytes and analyzers to build more suitable PBRTQC protocols.

Keywords
comparative assays, exponentially weighted moving average method, patient-based real-time quality control, quality management

Yide Lu and Fan Yang are contributed equally to this work

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1 | INTRODUCTION

At clinical laboratories, there is usually a great demand for the testing of biochemical samples. These tests may require the simultaneous use of multiple different models or brands of biochemical analyzers. The International Organization for Standardization (ISO) 15,189 standard specifies that a comparability scheme should be established to ensure the consistency of results. In routine practice, comparison assays with fresh serum samples and daily quality control (QC) samples, which are not commutable as patient samples with a material matrix, are recommended. However, this system is conducted at certain intervals rather than continuously, which increases potential quality risks during the analytical process. Patient data have potential advantages in aiding the implementation of laboratory management, particularly following the revolution of information technology. Nevertheless, the consideration of applying patient data in multi-analyzer comparisons is still underexplored.

The International Federation of Clinical Chemistry (IFCC) and the International Council for Clinical Chemistry and Analytical Quality in Laboratory Medicine proposed that patient-based real-time quality control (PBRTQC) is a valuable complementary quality control method, having the advantages of lower cost, absence of matrix effects, continuous real-time monitoring, and higher sensitivity to preanalytical errors. Various arithmetic procedures have been applied for PBRTQC, including Bull’s algorithm, the moving average (MA) method, and the exponentially weighted moving average (EWMA) method. To evaluate and monitor the comparability and stability of clinical tests across manufacturers and laboratories, the median of patient data is most widely used. However, this requires a large quantity of samples, and the performance is greatly affected when the amount of data is relatively small. In the EWMA algorithm, a weighting coefficient is introduced to smooth the dataset by adjusting the sensitivity of bias based on the training data. By using this method, which is reported to be less affected by sample size, small deviations in the process can be detected.

In this study, PBRTQC protocols using the EWMA algorithm were set up using the professional artificial intelligence software AI-MA. Then, we conducted comparison assays using the EWMA algorithm and the median method and evaluated the performance by comparing the results from serum samples. Overall, we attempted to establish a more convenient, economical, and efficient method for interanalyzer consistency monitoring in clinical laboratories.

2 | MATERIALS AND METHODS

2.1 | Analyzer and analytes

Three Beckman Coulter AU5800 series clinical chemistry analyzers (Beckman Coulter, United States) were used in the clinical laboratory at Ruijin Hospital, Shanghai Jiaotong University, School of Medicine, namely, AU5821_1, AU5821_2, and AU5800_3, which were marked as analyzers A, B, and C, respectively, in the present study. Eleven common analytes, including alanine aminotransferase (ALT), aspartate aminotransferase (AST), gamma-glutamyl transferase (GGT), alkaline phosphatase (ALP), creatine (CREA), uric acid (UA), potassium (K), sodium (NA), chloride (CL), calcium (CA), and inorganic phosphorus (PHOS), were studied using the three analyzers. In total, approximately 5000 samples were measured every day. Analyzers A and B were randomly assigned to run outpatient and inpatient samples, which were equivalent to approximately 2000 tests per day. Analyzer C was mainly used for urgent samples, averaging 500 and 200 tests for inpatient and outpatient samples, respectively. Three levels of internal quality controls (IQCs) were measured at the beginning of the analytical batch in the morning, and clinical sample testing was performed only when IQCs were in control. All of the IQC results were recorded and exported from the Beckman information system. Events that may have affected the analytical results, such as reagent lot changes, detection light calibrations, and reagent calibrations, were also recorded.

2.2 | Simulating and optimizing PBRTQC protocols based on the AI-MA platform

The process of establishing optimal PBRTQC protocols in the AI-MA platform is illustrated in Figure 1A. Briefly, raw data in the laboratory information system (LIS) containing measurand information were directly collected, extracted, and processed by using the AI-MA software version 1.0, which was developed by SENXU MEDICAL Corporation (Shanghai, China). By implementing multiple parameters for data investigation, a quality risk prediction model for PBRTQC was built through deep machine learning with the random forest method constructed from decision tree algorithms. The parameters, including the measurands, inclusion/exclusion of sample sources, specimen types, truncation limits, time windows, and smoothing factors, were set. The datasets for training and testing were proportionally extracted, and the PBRTQC model was established with multiple parameters. The EWMA algorithm is given as

\[ \text{EWMA}_t = (1 - \lambda) \text{EWMA}_{t-1} + \lambda \times x_t, \]

where \( \text{EWMA}_t \) and \( x_t \) are the estimated and actual values of the \( t \)-point measurement, respectively, and \( \lambda \) is the smoothing factor.

To obtain a stable dataset and avoid the deleterious effects of extreme values, we set truncation limits (TLs) based on biological variations (BVs) in the European Federation of Clinical Chemistry and Laboratory Medicine (EFLM) Biological Variation Database. The BVs of a measurand contained within-subject variations (CV\(_s\)) and between-subject variations (CV\(_b\)). The upper and lower TLs of the measurands were derived from the following formulas:

\[ \text{RCV}_G = 2.76 \times \sqrt{\text{CV}_G^2 + \text{CV}_I^2} \tag{1} \]

\[ \text{TLs} = \text{Means} \pm \text{RCV}_G \tag{2} \]
Here, \( \text{Means} \) represents the average value of the test results from all patients within the previous 6 months. If the amount of data in each group per day did not exceed 10, the data were excluded.

The control limits of the AI-MA EWMA chart were set based on the traditional concept of the Levey–Jennings graph using \( \bar{x} \pm 1, 2 \), and \( 3\sigma \) and were modified by the introduction of quality objectives. \( \bar{x} \) and SD represent the mean and standard deviation of the EWMA results accumulated in the previous 6 months, respectively. EWMA QC rules were applied based on the 10x and 4 1s “Westgard Rules” and machine learning of the control charts.

To verify the performance and select optimal protocols, we randomly selected a confirmed unbiased dataset and introduced positive/negative allowed total errors (TEa)\(^{14} \) for approximately 200–300 data points. Under different parameters, the data were resubmitted and calculated. The probability of error detection (Ped) and false-positive rate (FPR) was calculated based on the quality control chart. The optimal EWMA protocols were determined if Ped > 90\% and FPR < 5\%.

3 | COMPARATIVE ASSAYS BY SERUM SAMPLES AND PATIENT DATA FROM EWMA OR MEDIANS

The study design of the comparative assay is illustrated in Figure 1B. As the gold standard for interinstrument comparisons, measurement procedures were performed based on the Clinical and Laboratory Standards Institute (CLSI) EP9-A3 guidelines.\(^{15} \) Serum samples were collected and prepared according to an updated protocol based on Clinical and Laboratory Standard Institution (CLSI) C37-A.\(^{16} \) The analyte concentrations were more evenly distributed within the measurement range and covered the medical determination levels (MDLs) (Table S1), as suggested at https://www.westgard.com/decision.htm. At least 40 fresh samples for each analyte, 8 per day for 5 consecutive days, were included. Single outlying results were identified and removed by the extreme linearized deviation (ESD) method. Extra samples were added to reach a total of 40 samples if necessary. The Passing-Bablok analysis model using Medcalc software version 19.3 was used to obtain regression equations. The assessment of bias was determined by substituting medical determination levels into the equations and setting the acceptance limits as ½ allowed total errors (TEa).\(^ {17} \)

During the period of serum sample comparisons, patient data from the three analyzers were collected using the median and the PBRTQC method under optimal parameter settings. Raw data of patient specimens were divided into three groups, total patient (TP), inpatient (IP), and outpatient (OP) groups, according to the source of the patients. Pairwise comparisons were performed, that is, B vs. A, C vs. A, and C vs. B. Interanalyzer differences were assessed by calculating the delta percentage difference of two compared results.

To further investigate the application of patient data in real-time monitoring interanalyzer comparability, the cumulative results of the three instruments were collected daily using the EWMA and median methods, and events that may have affected test results, including changes in reagent lots and bottles, the calibration of lights and kits, and the maintenance and malfunction of analyzers, were recorded. Intraanalyzer bias was assessed by comparing the daily EWMA or median value to its target value accumulated over the previous 6 months. Interanalyzer differences were calculated as (maximum-minimum)/average \( \times 100\% \).\(^ {10} \) The acceptable bias limits of both the
intra- and interanalyzers were set to ½ TE. Inter- and intraanalyzer bias events were recorded. If interanalyzer deviation on a given day was due to bias caused by a certain instrument, the two events were considered the same; otherwise, they were calculated as two separate events. A true bias alarm suggested by patient data was determined in the presence of a corresponding quality event; otherwise, it was regarded as a false alarm.

4 | RESULTS

4.1 | Performance of the PBRTQC algorithms

Taking serum K as an example, two batches of positive and negative bias were introduced into the original data (Figure 2). The number of biases detected by the PBRTQC model on the AI-MA platform was recorded with various weighting coefficients (Table S2). Using the truncation limit helped to exclude extreme values and provided a more stable dataset for process monitoring. It was presumed that a better performance of PBRTQC could be achieved using this dataset than the dataset without truncation (Figure 2). After performing simulations with different smoothing factors, we chose a λ value of 0.03 for the optimal PBRTQC model, and a Ped of 91.54% and FRP of 0% were obtained (Table 1). Moreover, the number of patient results affected before error detection (NPed) was investigated under different EWMA parameters. The optimal PBRTQC model generated a smaller NPed (Table 1, Figure 2), indicating a better performance in detecting erroneous results in a timely manner. Accordingly, the parameters for other analytes were obtained and are listed in Table S3.

4.2 | Test comparability by serum samples

We conducted serum sample comparison testing from August 16, 2021, to August 20, 2021. Forty samples of each analyte were separately measured in the three analyzers without any outlying results. Regression analysis revealed that all of the analytes had good correlation coefficients ($r^2 > 0.99$) among the analyzers. Then, we assessed the bias in medical determination by pairwise comparisons to determine whether the deviation was acceptable. Table S1 provides a detailed overview of the comparative assay results by serum samples. In general, good comparability was achieved for analytes ALT, AST, CREA, UA, K, NA, CL, CA, and PHOS, as no unacceptable levels of bias were detected at either level of concentration for any of the manufacturers. However, for analytes ALP and GGT, significant bias was observed when using analyzer C, as increased test results occurred for these analytes at lower concentrations.

4.3 | Test comparability using patient data

Accordingly, we conducted comparison assays using patient data. Notably, Figure S1 shows that the test number for each analyte in analyzer C was distinct from the other two analyzers, as there was a smaller number of OP patients. To investigate whether the results were affected by the patients’ source, we analyzed the dataset used with analyzer A, which had an equivalent number for the IP and OP groups, under the respective optimal PBRTQC models. The accumulated EWMA values are listed in Table S4. For analytes ALP, GGT, UA, K, and CA, the differences between patients’ sources were found to exceed the applied limits. Concerning distinct sample numbers and sources, all analytes were categorized to evaluate the performance of patient data in the analyzer comparison. The pairwise comparative analysis results by EWMA were in good accordance with those by the median method in each group (Table 2). For analytes with good comparability by serum assays, such as AST, K, NA, CL, CA, and PHOS, the assessment of pairwise bias was also performed with desirable limits derived from the EWMA and median methods in each group. For measurements of analytes ALT and UA, the serological comparison was excellent, but the results were falsely lower using analyzer C on the OP group for ALT and on the TP group for UA. Discrepancies when applying the data derived from the OP group were not detected for analytes GGT and ALP, for which we observed considerable positive bias when using analyzer C.

4.4 | Application of patient data in the surveillance of analyzer comparisons

To assess the application of the PBRTQC models in real-time analyzer comparisons, the ALT analyte data from the TP and IP groups were studied based on the aforementioned results. During the monitoring period, IQCs at the three concentrations were all in controls (Figure S2). The intra- and interanalyzer deviations by day were plotted with their respective symbols and corresponding dates (Figure 3). Overall, 3 and 4 potential abnormal events were recorded when using EWMA on the TP and IP groups, among which 66.67% (2/3) and 100% (4/4) were identified as true, respectively. In contrast, 6 and 10 out-of-range bias events were recorded for the IP and TP groups, respectively, when using the median method; however, only 50% of them were considered true (Table 3). Generally, the method using the median value had a significantly higher false-positive rate than the EWMA method. Categorizing patients when using EWMA protocols can clearly improve the accuracy of unexpected bias detection by increasing the detection rate and decreasing the false-positive rate.

5 | DISCUSSION

In this study, we aimed to establish optimal PBRTQC models for commonly requested test samples and assess their potential role in comparability assays in daily work. Compared with the synchronous serological methods, the results showed that PBRTQCs could be applied as an efficient tool for monitoring test comparability and stability in laboratories.
With the continuous improvement of laboratory information systems and the development of “big data” technology, professional software for the PBRTQC models was exploited and improved, promoting the application of PBRTQCs in the quality management of clinical biochemistry.\(^8,18\) When setting up the PBRTQC protocols, it is essential to screen out parameters through data training and to select appropriate indicators to evaluate the performance of the model, which typically requires researchers with an academic background in computer science. Researchers have proposed algorithm optimization methods, including simulated annealing\(^19\) and grid searches,\(^18,20\) to enable laboratories to practically design PBRTQC procedures. In the present study, we used commercial AI-MA software to establish PBRTQC models by incorporating multiple parameters through a deep learning strategy, which was developed based on big data processing by artificial intelligence technology. Optimal PBRTQC protocols were further selected and evaluated. By
using the optimal PBRTQC protocols, the comparative results were concordant with those obtained with serum samples. In general, the application of the intelligent platform may aid inspectors in more effectively selecting the optimal model for the laboratory.

Even though truncation limits were applied, patient data used for real-time monitoring systems were often affected by multiple factors, such as fluctuations in sample numbers, different sources of specimens, heterogeneous patient populations, and specific clinical interventions. Caution is particularly needed in laboratories that employ multiple instruments to measure the same analyte. The study by Song et al. implied that classifying patient data according to sources of specimens and setting quality control rules in consideration of different groups could efficiently reduce the false-positive rate of PBRTQCs.

As influences within a group were relatively limited and did not interfere with other groups, we divided the truncated data into the inpatient (IP), outpatient (OP), and total patient (TP) groups. The negative bias detected for analyte UA when using analyzer C for the TP group was probably false, as comparative results from both serum samples and categorized patient data were excellent (Table 2). Samples run using analyzer C consisted of a major composition of inpatient samples (Figure S1). Lower results for analyte UA were observed for these samples than for those from the outpatient groups (Table S4). Thus, we speculate that the false-negative bias was likely related to the inconsistent sample numbers and deviated patient data in different groups. In addition to analyte UA, accumulated patient data for analytes ALP, GGT, K, and CA differed between the OP and IP groups. Except for analytes ALP and GGT, which were detected as having true bias, the effects from group variations for analytes K and CA might have leveled off due to the large sample quality; thus, the data in the TP group were not influenced by the aforementioned factors. In addition, in the real-time monitoring of instrument comparability, we found that better performance in detecting small interinstrument variability and decreasing false-positive alarms was achieved using the categorized patient data. Thus, categorizing patients will be of great benefit to improve the performance of PBRTQC in comparative assays.

However, categorizing patients might lead to a decreased sample number, thus requiring further attention due to inherent limitations. For analytes with large between-subject biological variation (CV$_G$), the ability of PBRTQC to detect potential deviations was dramatically weakened on account of a smaller sample size and larger population variations. Likewise, for analytes ALT, ALP, and GGT, of which CV$_G$ was ranked highest, we observed false-positive and negative biased events for the OP group when using analyzer C. Nevertheless, for the analytes with relatively narrow biological variation, the desired performance was still achieved regardless of changes in sample size and patient categories. These findings emphasize the significance of considering the potential influences of low- and medium-sized populations, especially for highly varied analytes. Therefore, we suggested that PBRTQCs could be improved in relation to the sample size, population variation, and preanalytical factors for some specific analytes.

Another notable finding was that the deviated analytes were only observed when using analyzer C, which was operated 24 h a day for urgent samples. This nonstop running may have accelerated the consumption of the light source and aged the system, contributing to the instability of test samples. Enzymatic assays were particularly sensitive to manufacturing conditions, including temperature fluctuations and defective lamps, which is consistent with the results that showed that analytes ALP and GGT were significantly biased when using analyzer C. In this case, the laboratory should be aware of solving this issue through more frequent calculations and earlier replacement of light sources.

TABLE 1 Performance of PBRTQCs for serum K with different limits and smoothing factors

| Truncation Limits (mmol/L) | Smoothing factor | Introduced biased data | True detected biased data | False detected biased data | Ped (%) | FPR (%) | NPed |
|---------------------------|-----------------|-----------------------|--------------------------|---------------------------|---------|---------|------|
| 2.8–6.2                   | 0.01            | 550                   | 176                      | 262                       | 33.85   | 13.70   | —    |
|                            | 0.03            | 550                   | 476                      | 1032                      | 91.54   | 53.95   | —    |
|                            | 0.05            | 550                   | 476                      | 1194                      | 95.20   | 62.42   | —    |
|                            | 0.10            | 550                   | 56                       | 115                       | 11.20   | 6.01    | —    |
|                            | 0.20            | 550                   | 43                       | 93                        | 8.60    | 4.86    | —    |
|                            | 0.40            | 550                   | 47                       | 105                       | 9.40    | 5.49    | —    |
| 3.2–4.9                    | 0.01            | 550                   | 0                        | 0                         | 0.00    | 0.00    | 18   |
|                            | 0.03$^b$        | 550                   | 476                      | 0                         | 91.54   | 0.00    | 5    |
|                            | 0.05            | 550                   | 476                      | 203                       | 91.54   | 10.61   | 9    |
|                            | 0.10            | 550                   | 245                      | 559                       | 47.12   | 29.22   | 13   |
|                            | 0.20            | 550                   | 40                       | 32                        | 7.69    | 1.67    | 16   |
|                            | 0.40            | 550                   | 39                       | 3                         | 7.50    | 0.16    | 27   |

Abbreviations: FPR, false-positive rate; K, potassium; NPed, number of patient results affected before error detection; Ped, probability of error detection; PBRTQC, patient-based real-time quality control.

$^a$Not applicable.

$^b$Optimal PBRTQC factors are marked in bold.
**TABLE 2** Results of the pairwise comparison of analyzers by serum assays and patient data

| Analytes | % TEa (%) | Serum | TP | IP | OP |
|----------|-----------|-------|----|----|----|
|          |           |       | EWMA | Median | EWMA | Median | EWMA | Median |
|          |           |       | B vs. A | C vs. A | C vs. B | B vs. A | C vs. A | C vs. B | B vs. A | C vs. A | C vs. B | B vs. A | C vs. A | C vs. B |
| ALT      | 8.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          |           |       | −0.60 | 0.20  | 0.80  | 0.00 | 0.00 | 0.00 | −0.36 | 3.44  | 3.81  | 0.00 | 5.00 | 5.00 |
| AST      | 7.50      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 1.60      | 4.38  | 2.72  | 4.55 | 4.55  | 0.00 | 2.83 | 7.09 | 4.09 | 4.54  | 7.20  | 4.34 | 1.55 | 4.34 |
| ALP      | 9.00      | —     | ↑     | ↑    | ↑    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | −1.66     | 12.55 | 14.46 | −1.35 | 13.51 | 15.07 | −2.00 | 11.30 | 13.58 | −2.67 | 12.00 | 15.07 | −2.29 | 4.61 |
| GGT      | 5.50      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 2.39      | 17.87 | 15.12 | 4.54 | 18.18 | 13.04 | 2.60 | 11.60 | 8.84  | 0.00  | 12.00 | 12.00 | 2.20 | 6.67 |
| CREA     | 6.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 0.39      | −1.38 | −1.75 | 0.00 | −2.78 | −2.78 | 0.91 | −4.2 | −5.06 | 1.35  | −4.11 | −5.41 | −0.63 | −0.75 |
| UA       | 6.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 0.70      | −6.12 | −6.21 | 0.64 | −6.47 | −7.07 | −0.14 | −2.53 | −2.39 | −1.03 | −3.62 | −2.61 | 1.19 | −1.97 |
| K        | 3.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 1.25      | −1.50 | −2.72 | 1.51 | −1.26 | −2.72 | 1.28 | 0.00 | −1.26 | 1.02  | −0.26 | −1.27 | 0.97 | −2.43 |
| NA       | 2.50      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 0.01      | −0.33 | −0.23 | 0.00 | −0.71 | −0.71 | −0.03 | −0.26 | −0.23 | 0.00  | −0.71 | −0.71 | 0.06 | −0.03 |
| CL       | 2.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 0.06      | 0.07  | 0.01  | 0.00 | 0.00  | 0.00 | 0.05 | 0.09 | 0.04 | 0.00  | 0.00  | 0.00 | −0.13 | 0.48 |
| CA       | 2.50      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | 2.21      | 1.77  | −0.43 | 2.20 | 1.76  | −0.43 | 1.34 | 2.23 | 0.88 | 0.44  | 1.33  | 0.88 | 2.16 | 2.16 |
| PHOS     | 5.00      | —     | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    | —    |
|          | −0.00     | −3.60 | −3.60 | 0.00 | −3.60 | −3.60 | 0.00 | −2.72 | −2.72 | −0.90 | −2.70 | −1.82 | 0.00 | 0.89 |

Abbreviations: ALP, alkaline phosphatase; ALT, alanine aminotransferase; AST, aspartate aminotransferase; CA, calcium; CL, chloride; CREA, creatine; EWMA, exponentially weighted moving average; GGT, gamma-glutamyl transferase; IP, inpatient population; K, potassium; NA, sodium; OP, outpatient population; PHOS, inorganic phosphorus; TEa, allowed total errors; TP, total population; UA, uric acid.

A, B, and C indicate analyzer A, B, and C, respectively.

*Increased data value.

**Significant differences are underlined in bold.

*No significant difference.
Since IQC and serum samples hardly reflect the stability of the detection system in the whole process, we then aimed to use the optimal EWMA and median methods to monitor the fluctuation of the inter- and intraanalyzers. The EWMA algorithm appeared to perform much better than the median method in the application of daily monitoring analyzer stability, even though both methods exhibited similar performance on comparative assays. The deficiencies of the median method that led to a higher FPR became prominent when using applied patient data per day other than those from five accumulated days for comparative assays. As suggested by Kenneth Goossens on the “The Percentiler” project,10 the median method was greatly affected by population variations in small- and medium-sized samples. Therefore, PBRTQC protocols with the EWMA algorithm were more suitable as an efficient tool for the real-time monitoring of analyzer comparability and stability. However, we found that we were more likely to detect very small changes in the detection systems, for example, kit lot variations and light calibration, when the IQCs were all in controls, and the PBRTQCs were used. We recommend that PBRTQCs, especially with an EWMA algorithm, be conducted as a supplementary procedure to expand the application of analyzer comparability to guarantee the performance of laboratory detection systems.

However, there are some limitations in our study. First, we set up individual optimal PBRTQC models with combined patient data other than the data from the analyzers. As stated by Zhou et al.24 the performance of PBRTQC could be better if data were applied using separate instruments. In addition, in the simulation process, the intellectual QC rules to assess the biased data points in the chart were built in the software and were confidential for the corporation. Finally, we monitored the stability of the analyzers for a relatively short period of 1 month and only for the analyte ALT; this study should be continued for a longer time and for more analytes. In general, further studies should be conducted to optimize and expand the application of PBRTQC.

**Figure 3** Surveillance of comparability and stability of inter- and intraanalyzers for alanine aminotransferase (ALT) by (A) the EWMA method with data from the total population (TP) (B) the EWMA method with data from inpatients (IP) (C) the median method with data from TP and (D) the median method with data from IP. A, B, and C indicate analyzers A, B, and C, respectively. Unacceptable biases for intraanalyzers were pointed out with circles for analyzer A, squares for analyzer B and triangles for analyzer C in the chart. Significant deviations for interanalyzers were marked by underlining its relevant dates. Abbreviation: EWMA, exponentially weighted moving average.
Yide Lu and Fan Yang designed the study and proposed the application of PBRTQC; Dongmei Wen supported the data analysis; Kaifeng Shi and Zhichao Gu collected the data and recorded cases; Qiuya Lu reviewed and revised the article; Xuefeng Wang supervised the study and reviewed the article; Danfeng Dong designed and wrote the article. All of the authors read and approved the final article.

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Danfeng Dong https://orcid.org/0000-0002-1023-202X

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SUPPORTING INFORMATION
Additional supporting information can be found online in the Supporting Information section at the end of this article.

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