Magnetic resonance vessel wall imaging in cerebrovascular diseases

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Cerebrovascular diseases manifest as abnormalities of and disruption to the intracranial vasculature and its capacity to carry blood to the brain. However, the pathogenesis of many cerebrovascular diseases begins in the vessel wall. Traditional luminal and perfusion imaging techniques do not provide adequate information regarding the differentiation, onset, or progression of disease. Intracranial high-resolution MR vessel wall imaging (VWI) has emerged as an invaluable technique for understanding and evaluating cerebrovascular diseases. The location and pattern of contrast enhancement in intracranial VWI provides new insight into the inflammatory etiology of cerebrovascular diseases and has potential to permit earlier diagnosis and treatment. In this report, technical considerations of VWI are discussed and current applications of VWI in vascular malformations, blunt cerebrovascular injury/dissection, and steno-occlusive cerebrovascular vasculopathies are reviewed.

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1995, when investigators reported age-related changes in the degree of carotid artery (CA) and vertebral artery (VA) contrast enhancement.2 VWI has since been applied to the evaluation of cerebrovascular conditions including cerebral aneurysms, post–subarachnoid hemorrhage (SAH) vasospasm, traumatic blunt cerebrovascular injury (BCVI), and other steno-occlusive conditions.29,37

Technical Aspects

To accurately characterize lesions within thin vessel walls, a high contrast-to-noise ratio (CNR) and spatial resolution are critical. The CNR is the signal contrast between the vessel wall and the surrounding luminal blood and CSF. Suppression of luminal blood depends on intrinsic “black blood” quality of 2D and 3D acquisition sequences. The vessel wall should be visualized in multiple axes. Using multiple orthogonal 2D sequences is one

ABBREVIATIONS ACoA = anterior communicating artery; AVM = arteriovenous malformation; BCVI = blunt cerebrovascular injury; CA = carotid artery; CNR = contrast-to-noise ratio; CTA = CT angiography; DANTE = delayed alternating nutation for tailored excitation; DSA = digital subtraction angiography; ICA = internal carotid artery; MCA = middle cerebral artery; MMD = moyamoya disease; MMS = moyamoya syndrome; MRA = MR angiography; MSDE = motion-sensitized driven equilibrium; PCoA = posterior communicating artery; PHASES = population, hypertension, age, size of aneurysm, earlier SAH from another aneurysm, and site of aneurysm; RCVS = reversible cerebral vasoconstriction syndrome; SAH = subarachnoid hemorrhage; SPACE = sampling perfection with application-optimized contrasts by using different flip angle evolutions; VA = vertebral artery; VISTA = volume isotropic turbo spin echo acquisition; VWCE = vessel wall contrast enhancement; VWI = vessel wall imaging.

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FIG. 1. Optimized blood and CSF suppression to reduce artifacts in VWI. Suppression of artifacts is important in VWI. DANTE is a preparation pulse that suppresses CSF and blood flow signal (A and B). Eccentric vessel wall enhancement is seen in both DANTE (A, bold arrow) and non-DANTE (C, bold arrow) sagittal T1 SPACE VWI, representing intracranial atherosclerosis. However, DANTE suppresses nonspecific enhancement in a vein (B, curved arrow), which enhances on the non-DANTE sequence (D, arrow).

method, but partial volume averaging can obscure the arterial wall’s appearance. With 2D VWI, double inversion recovery pulses can be used to generate blood flow suppression. Spin-echo imaging techniques inherently also generate dark luminal blood, but are limited by slow or in-plane flow resulting in loss of suppression.29

Newer 3D VWI volumetric acquisitions enable increased brain coverage and through-plane resolution, with isotropic scans reformatted in multiple planes. These include variable refocusing flip angle sequences (VRFA), with T1 or proton density-weighted pre- and postcontrast sequences, such as volume isotropic turbo spin echo acquisition (VISTA; Philips Healthcare), sampling perfection with application-optimized contrasts by using different flip angle evolutions (SPACE; Siemens), and Cube software (GE Healthcare). Preparation pulses, such as motion-sensitized driven equilibrium (MSDE), which uses flow-sensitive dephasing gradients, also achieve blood suppression. Another approach to optimize blood and CSF suppression is delayed alternating nutation for tailored excitation (DANTE), a preparation pulse that uses a series of low flip angle nonselective pulses interleaved with gradient pulses of short repetition times.18,32,37,63

Laminar blood flow through pathological segments is often slow, turbulent, or stagnant. Vessel wall contrast enhancement occurs at sites of pathological instability and inflammation. However, because gadolinium shortens T1 relaxation time, “black blood” suppression in areas of abnormal or even normal in-plane flow can be diminished. This potentially causes an artifact of unsuppressed contrast in flowing blood, appearing as vessel wall contrast enhancement (VWCE). This is seen with turbulence and recirculation within aneurysm sacs, slow flow within dilated lumens, and retrograde filling of distal collateral branches with proximal occlusion.32 This can also be seen in certain arterial segments in healthy patients on postcontrast 3D VWI, specifically with in-plane arteries. DANTE preparation pulses suppressed near-wall enhancement by 50% compared to 3D turbo spin echo alone, underscoring the significance of artifact and the value of preparation pulses (Fig. 1).26

Other sources of misinterpreted VWCE include vasa vasorum, adjacent veins, and endovascular interventions such as mechanical thrombectomy.32 With age-dependent atherosclerosis, the extracranial vasa vasorum network can extend into the proximal intracranial arteries to supply stenotic vessels.2 This phenomenon can also happen distally, with smaller intracranial branches supplying the adventitia of larger, stenotic vessels. This can appear as concentric (circumferential) VWCE and can mimic inflammatory vasculitis. The differentiating feature between vasa vasorum and inflammatory vasculopathy is the lack of arterial stenosis and wall edema with vasa vasorum ingrowth. Veins traveling adjacent to the artery of interest may appear as VWCE on 2D VWI, but this is not typically a problem with 3D VWI. Imaging in a second orthogonal plane can clarify this. Recanalization of occluded arteries after mechanical thrombectomy causes concentric VWCE, similar in appearance to inflammatory vasculitis, probably secondary to arterial wall injury, and has associations with longer procedures with multiple passes and subsequent hemorrhagic conversion.32,56

Scanning at higher field strengths in which 3D VWI techniques are used provides improved through-plane resolution, signal-to-noise ratio, imaging reproducibility, and CNR. CSF flow can result in artifacts that can mimic arterial wall abnormalities. Incorporating an antidriven equilibrium pulse at the end of the echo train to a 3D turbo spin echo acquisition can reduce tissue signals with long T2 relaxation times, such as CSF, independent of flow. Augmentation with antidriven equilibrium provides 50% improvement in the M1 segment and 183% improvement in the basilar artery for wall-to-CSF CNR.27 DANTE preparatory pulses can also suppress CSF signal and flow artifacts when used with 3D VWI techniques.68

Intracranial vessel walls are challenging to image due to their tortuosity and small caliber. The thickness of the proximal middle cerebral artery (MCA) wall varies from 0.4 mm to 0.7 mm, with a mean outer diameter of 3.4 mm.1,46 A recent ex vivo study of VWI of the circle of Willis showed accurate reliability comparing histological and 7-T MR measurements across entire arterial segments.22 Currently, a resolution of 3 T (0.4- to 0.5-mm isotropic voxel size) is preferred in the clinical setting—balancing cost, acquisition time, image quality, diagnostic accuracy, and clinical need.29
In 2018, the American Society of Neuroradiology formulated guidelines for the applications of VWI. The current consensus advocates for pulse sequences sufficient for blood and CSF suppression, 2D sequences in short- and long-axis planes, and 3D sequences with isotropic voxel dimensions and multiplanar reformatting.

**Current Applications of VWI**

**Vascular Malformations**

**Cerebral Aneurysms**

Cerebral aneurysms are the manifestation of different pathological processes involving the intracranial cerebral vessel wall. Traditional imaging, including DSA, informs luminal caliber and alterations to intracranial blood flow. For evaluation of saccular aneurysms, this provides anatomical information including size and location, forming the basis for risk quantification systems such as the population, hypertension, age, size of aneurysm, earlier SAH from another aneurysm, and site of aneurysm (PHASES) classification system. However, aneurysm size-based scoring systems are imperfect because the majority of ruptured aneurysms are small.

VWCE reflects the degree of vessel wall inflammation, which is characterized by vessel wall thickening, development of vasa vasorum, and macrophage infiltration. VWI provides information regarding 1) stability of the aneurysm wall and risk of aneurysm rupture, and 2) discrimination between ruptured and unruptured aneurysms (in a patient with multiple aneurysms). VWI of aneurysm walls has demonstrated increased enhancement in growing and recently ruptured aneurysms. VWCE has been correlated with inflammatory changes at a histological level, and has been associated with inflammatory vasculopathies such as mycotic aneurysms and HIV-associated vasculitis.

**Multiple Cerebral Aneurysms.** When a patient with multiple intracranial aneurysms presents with acute SAH, the offending aneurysm may not be easy to identify. However, aneurysm rupture is associated with VWCE with high sensitivity and can be used to identify the ruptured aneurysm, facilitating surgical decision-making (Fig. 2). After the initial report by Matouk et al., subsequent studies have examined more than 500 aneurysms and found that >95% of ruptured aneurysms demonstrated enhancement. Approximately 25% of unruptured aneurysms also demonstrated enhancement; many of them were deemed unstable based on documented growth or symptoms. These results suggest that VWI has a high sensitivity and negative predictive value for identifying acute ruptured aneurysms.

**Stability of Cerebral Aneurysms.** Unstable aneurysms are at higher risk of rupture and warrant treatment. Stability is based on aneurysm size, morphology, documented growth, and/or clinical symptoms. In addition to established risk-quantification strategies such as the PHASES score, VWI provides an additional method to evaluate aneurysm stability.

![FIG. 2. Contrast enhancement in VWI identifies the ruptured aneurysm. A patient presented with high-grade SAH (A) and multiple aneurysms on angiogram; a left posterior cerebral artery (PCA) dissecting aneurysm (B, arrow) and an ACoA aneurysm (F, arrow). VWI demonstrates significant wall enhancement involving the PCA aneurysm (C) suggesting this as the source of SAH. The white boxed area is enlarged in D; arrow designates the PCA aneurysm. The unruptured ACoA aneurysm does not enhance more than the surrounding arterial walls (G). The white boxed area is enlarged in H; arrow designates the ACoA aneurysm. The patient underwent successful endovascular coiling of the ruptured left PCA aneurysm (E, arrow).](image-url)
with high-risk features and instability in unruptured aneurysms. In 140 unruptured aneurysms, VWCE was associated with greater mean aneurysm size (10.4 vs 5.6 mm) and a higher-risk location (anterior communicating artery [ACoA], posterior communicating artery [PCoA], and posterior circulation). In one study, 92.3% of aneurysms with a PHASES score > 10 were enhanced compared with 33.9% of aneurysms scoring < 4. Similarly, dichotomizing 45 patients into PHASES scores of either ≥ 3 or < 3, our group reported VWCE in 42.1% versus 14.8%, respectively.

There are limitations to this application. VWI and VWCE patterns may be misleading, with both false positives and false negatives for evaluating aneurysm rupture. In one reported case, a patient with acute SAH was found to have 2 lesions: a 3.5-mm MCA aneurysm and a 1.5-mm PCoA aneurysm. On VWI, the MCA aneurysm demonstrated circumferential enhancement, whereas the PCoA aneurysm did not enhance. Intraoperatively, the PCoA aneurysm was found to be acutely ruptured, in contradiction to the VWI result.

The significance of VWCE in unruptured aneurysms without obvious unstable features remains unclear. This is a clinically important group, because these aneurysms are often observed. Future studies will need to examine whether VWCE in this so-called low-risk group is predictive of instability and higher risk of rupture, thereby warranting prompt treatment.

Vasospasm. VWI may predict and detect vasospasm following SAH and aneurysm treatment. In a cohort of unruptured and ruptured aneurysms in which VWI was obtained soon after endovascular treatment (prior to the classic onset of vasospasm and delayed cerebral ischemia), early VWCE in second- and third-order intracranial arteries was significantly associated with development of angiographic vasospasm, even after controlling for modified Fisher grade (Fig. 3). Intracranial arterial segments were also more likely to show enhancement following aneurysm rupture and modified Fisher grade 4 SAH. It is possible that VWCE reflects inflammatory changes that are more robust following aneurysm rupture and high-grade aneurysmal SAH, correlating with the risk of developing vasospasm. Although the extent of SAH is the most reliable predictor of vasospasm, the clinical severity of vasospasm varies considerably and can occur even with low-grade SAH. VWI may have a valuable role in the prediction of vasospasm in otherwise low-risk patients.

Follow-Up of Flow-Diverter–Treated Aneurysms. VWCE is frequently seen following balloon- or stent-assisted endovascular treatment or deployment of flow diverters. Although the mechanism of VWCE is unclear, it probably represents mechanical irritation that resolves over time, and is thought to be related to an inflammatory process in the vessel wall and the transient breakdown of the blood-brain barrier. Posttreatment VWCE does not appear to be associated with instability and increased risk of aneurysm rupture. Further study is needed to determine whether VWCE, either at the time of treatment or at long-
Subintimal dissections communicate with the lumen and are often associated with stenosis of the artery and thromboembolism. Subadventitial dissections may lead to pseudoaneurysm formation, with risk of rupture and SAH. Due to the absence of external elastic lamina and a thinner adventitial layer in the intradural vasculature, intracranial dissections tend to occur in the subadventitial plane. Angiography may incompletely image these lesions, particularly if there is minimal arterial stenosis or the false lumen is thrombosed (Fig. 4).58

High-resolution VWI may help delineate important anatomical details or reveal lesions not evident with other imaging modalities.11 Typical findings include a dissection flap, an intramural thrombus, and abnormal enhancement. Dissection flaps may not be detected reliably,43 but intramural hematomas are seen in 87%–100% of cases.10,29,43,61,62 Detection is aided by the inclusion of susceptibility-weighted and noncontrast T1-weighted sequences.10,29 The majority are hyperintense on T1- and T2-weighted sequences (74% and 60%, respectively), with the remainder demonstrating iso- or hypointense signal intensity on T1- and T2-weighted sequences. As with intracerebral hematomas, the signal characteristics of intramural hematomas change predictably with time. Thus, MRI appearance can define the chronicity of the injury.21

VWCE is evident in approximately two-thirds of dissections.3,14,47,61 When present, this finding is thought to be due to inflammation, stasis of blood within the false lumen, or disruption of the vasa vasorum.48,50 The enhancement pattern tends to be eccentric (< 50% circumference),48,61 and may extend beyond the visualized dissection flap and/or hematoma, suggesting farther-reaching injury to the intima than can be seen on noncontrast sequences (Fig. 4).3 Extensive enhancement in cervical dissections may be associated with a heightened risk of multiple dissections and stroke, raising the question of whether these patients have a more severe vasculopathy.14,47 However, VWCE is not a specific indicator of dissection, because this finding can be seen in areas without other evidence of vessel pathology.3 Whether this represents an underlying vasculopathy that predisposes to dissection remains unclear.

Arteriovenous Malformations

The results from A Randomized Trial of Unruptured Brain Arteriovenous Malformations (ARUBA) support the nonsurgical treatment of unruptured high-grade arteriovenous malformations (AVMs).36 However, when an AVM presents with acute hemorrhage, it is reasonable to identify high-risk features, such as intranidal and flow-related aneurysms that may be the source of the hemorrhage, and to target these lesions for intervention.25 Identification and treatment of the rupture point in a high-grade complex AVM is often difficult. In several reports, VWI has demonstrated promise in identifying the rupture point by the presence of significant VWCE.24 Additional evidence is required prior to widespread clinical adoption, however.

Dissection and BCVI

CA and VA Dissection

Spontaneous arterial dissections are an important cause of stroke especially in young patients.52,58 and VWI may facilitate identification and characterization of these lesions. CA and VA dissections occur intracranially and extracranially.52,58 Dissections occur when a tear in the intimal layer allows blood under arterial pressure to elevate a subintimal and/or subadventitial flap, creating a false lumen and an associated intramural hematoma.52 Dissections and the associated hematoma can cause stroke by stenosis of the artery, occlusion of the branching vessels’ ostia, or formation of arterial thromboemboli.52

Blunt Cerebrovascular Injury

Traumatic injury to the CA or VA is a major cause of stroke, especially in younger patients. As many as 2.4% of patients admitted with nonpenetrating trauma have radiographic evidence of BCVI; of these, 5%–10% experience a stroke.5,13,54,55,60 CTA is commonly used to screen at-risk trauma patients with excellent sensitivity.16,59 However, false-positive findings are common, particularly in low-grade injuries, where the positive predictive value of CTA is only 30%.19 Furthermore, as many as 42% of BCVIs identified with CTA are equivocal; of these 36% remain indeterminate on delayed repeat CTA.15 Given the risks of treatment with antiplatelet and antithrombotic agents, avoiding overdiagnosis is important. Although DSA remains the gold standard, this test is invasive and not without risk. VWI may help improve diagnostic accuracy in at-risk patients. A small pilot study found that VWI of-
ferred significantly better discrimination between equivocal findings and true BCVI, particularly in low-grade lesions. Further research will be needed to better delineate the role of VWI in this population.

**Steno-Occlusive Cerebrovascular Vasculopathies**

**CA and Intracranial Atherosclerosis**

VWI provides a supplementary method for early diagnosis of intracranial and extracranial atherosclerosis and to target at-risk atherosclerotic lesions. Current treatment algorithms may be based on luminal stenosis, with symptoms and 70% stenosis of the extracranial carotid artery used as the threshold for endovascular treatment or carotid endarterectomy. However, VWI shows that high-risk atherosclerosis may not always be associated with significant stenosis. Angiography can underestimate the atherosclerosis burden, and does not detect nonstenotic lesions. VWI directly evaluates plaque, particularly the degree and pattern of vessel wall thickening. Indeed, increases in arterial VWCE correlate with age and atherosclerosis progression. The typical atherosclerosis plaque is an eccentric, heterogeneous, contrast-enhancing, positive remodeling lesion (Fig. 5). Positive remodeling with an increase in vessel wall thickness as a compensatory dilatation, without initial changes in lumen diameter, can be missed by luminal imaging until later stages when stenosis occurs. Plaque rupture is often apparent at sites with only modest luminal stenosis but significant positive remodeling. Arteries with positive remodeling are more vulnerable to rupture than those with negative remodeling. With significant positive remodeling, chronic hypoperfusion may occur in the absence of significant stenosis.

The layered pathological structure of atherosclerotic plaques resected via carotid endarterectomy correlates with VWI appearance. These specimens have juxtaluminal fibrous caps, lipid cores, and increased vasa vasorum ingrowth. Radiographically, these are demonstrated by a T2-hyperintense and T1-enhancing juxtaluminal layer, a T2-isointense, T1-hypointense nonenhancing middle layer, with a variable thickness enhancing outer layer, respectively. With increasing volume of a necrotic lipid core, there is an increased risk of rupture. In multifocal atherosclerotic disease, culprit lesions enhance more consistently than nonculprit lesions. The radial location of plaques along vessel walls can forecast stroke type. For example, plaques along the superior wall of the MCA are associated with lenticulostriate infarcts. Intraplaque hemorrhage has been shown to be one of the strongest markers for plaque vulnerability, and is represented by T1 shortening within the plaque.

Adding VWI to luminal imaging allows differentiation of atherosclerosis from other nonocclusive vasculopathies. In a recent study in which atherosclerosis, vasculitis, and reversible cerebral vasoconstriction syndrome (RCVS) lesions were evaluated, the addition of VWI to luminal imaging increased diagnostic accuracy from 43.5% to 96.3% compared with luminal imaging alone. Furthermore, 91% of atherosclerotic lesions were found to have an eccentric enhancing pattern, as opposed to the concentric enhancement found in vasculitis or RCVS. VWI has also shown reliability in interrater and interscan reproducibility for atherosclerotic plaque identification intracranially.

**Moyamoya Vasculopathy**

Moyamoya disease (MMD) is an idiopathic bilateral narrowing of internal carotid artery (ICA) termini leading to chronic hypoperfusion and risk of hemorrhage. Moyamoya syndrome (MMS) is the unilateral or bilateral supraclinoid ICA stenosis secondary to vasculopathies including intracranial atherosclerosis, vasculitis, radiation, and neurofibromatosis. Pathological changes of MMD include fibrocellular thickening of the intima, including hyperproliferation of the vessel wall, active angiogenesis, and matrix accumulation. A small number of inflammatory cells are seen on histological studies. There is also irregular undulation of the internal elastic laminae, attenuation of the media, and a decrease in the outer diameter of the vessel.

It is important to distinguish MMD from MMS, because MMD usually requires surgical revascularization. This is in contrast to MMS, where the underlying causes may be reversible with medication. Luminal imaging cannot reliably distinguish between MMD and MMS. On
VWI, MMS secondary to vasculopathy such as atherosclerosis will typically show focal eccentric lesion enhancement and outward remodeling (Fig. 6E–H). In contrast, segments affected by MMD tend to rarely enhance with no outward remodeling (Fig. 6A–D). When MMD segments do enhance, they have a mild concentric, homogeneous pattern. Another study directly comparing MMD and atherosclerotic vessel walls found bilateral distal ICA concentric enhancement and MCA wall shrinkage to be characteristic of MMD.8

VWCE in MMD may be an indicator of evolving intimal hyperplasia, neovascularization, and transient underlying inflammation correlating with disease instability and poor clinical outcomes. A recent cross-sectional study of 51 symptomatic patients with MMD found that patients with the highest degree of concentric VCWE had a higher incidence of acute ischemic stroke. The patient group with the highest enhancement had a 76% occurrence of acute ischemia, whereas the groups with minimal or no enhancement had 50% and 48%, respectively. However, the study did not distinguish between patients with MMD versus those with MMS, and included patients with unilateral and bilateral disease. Future prospective studies are needed to evaluate the clinical utility of VWI in differentiating MMD and MMS, and for predicting ischemic and hemorrhagic events, which could help stratify low- and high-risk patients and guide management decisions.

CNS Vasculitis

Conventional angiography may not be sensitive enough to detect the subtle changes in the distal cerebral vasculature affected by inflammatory vasculitis. VWCE in inflammatory vasculitis is theorized to be secondary to endothelial permeability and contrast leakage. VWI has shown the ability to detect small artery inflammatory vasculopathies. Contrast-enhanced MRI can detect enhancement in the parenchyma adjacent to the adventitia, representing inflammatory spillover, increasing the detection of affected segments, and may serve as an indicator of pathological microvascular involvement. On VWI, inflammation and edema within the vessel wall will show thickening and multifocal, homogeneous, and concentric enhancement. This is particularly useful for detecting a treatment response of presumed vasculitis after immunosuppressants. VWI may decrease the need for a high-risk brain tissue biopsy for CNS vasculitis, which has inherently low sensitivity. If a biopsy is indicated, VWI may help target a potentially high-yield lesion.

FIG. 6. VWI in MMD (A–D) and MMS (E–H). In MMD there is asymmetrical narrowing of the bilateral ICA terminus (arrows) and proximal anterior cerebral artery (ACA) and MCA (A). On T2-weighted VWI (B), there is no evidence of appreciable wall thickening. On T1-weighted pre- and postcontrast VWI (C and D, respectively), there is no evidence of outward remodeling, appreciable wall thickening, or wall signal abnormality. In MMS secondary to atherosclerosis, there is irregularity and asymmetrical cavernous and supraclinoid ICA stenosis (E, arrow). On axial T2-weighted VWI (F) there is wall thickening, with juxtaluminal T2 hyperintensity for the atherosclerotic fibrous cap and subjacent hypointensity for the lipid core (arrow). On T1-weighted pre- and postcontrast sagittal oblique VW images (G and H, respectively), there is outward remodeling plaque showing enhancement involving the CA terminus and ACA (arrows).
Reversible Cerebral Vasospasm Syndrome

RCVS presents with sudden, severe headache and concomitant neurological deficits. Affected patients can develop infarction, SAH, edema, and intraparenchymal hemorrhage. In RCVS, VVI shows minimal smooth, concentric thickening with minimal diffuse or no enhancement. This appearance is consistent with the syndrome’s pathophysiology, a noninflammatory transient vasospasm, and distinguishable from other causes of nonstenotic intracranial stenosis. A disproportionately greater increase in stenosis relative to the wall thickening is characteristic of vasospastic arteries. RCVS will show complete luminal resolution after approximately 3 months with conservative treatment. This contrasts with CNS vasculitis, which will usually demonstrate persistent VWCE and luminal narrowing despite treatment.

Conclusions

High-resolution MR VWI complements traditional luminal and perfusion studies in the evaluation of cerebrovascular disease, and may allow earlier diagnosis and treatment, differentiate disease processes, and facilitate longitudinal evaluation. The clinical application for VVI is wide-ranging, answering important clinical questions and informing management decisions. Future prospective studies should be conducted to confirm the clinical benefit and accuracy associated with this imaging modality.

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