Effects of Mucin and DNA Concentrations in Airway Mucus on *Pseudomonas aeruginosa* Biofilm Recalcitrance

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**ABSTRACT** The pathological properties of airway mucus in cystic fibrosis (CF) are dictated by mucus concentration and composition, with mucins and DNA being responsible for mucus viscoelastic properties. As CF pulmonary disease progresses, the concentrations of mucins and DNA increase and are associated with increased mucus viscoelasticity and decreased transport. Similarly, the biophysical properties of bacterial biofilms are heavily influenced by the composition of their extracellular polymeric substances (EPS). While the roles of polymer concentration and composition in mucus and biofilm mechanical properties have been evaluated independently, the relationship between mucus concentration and composition and the biophysical properties of biofilms grown therein remains unknown. *Pseudomonas aeruginosa* biofilms were grown in airway mucus as a function of overall concentration and DNA concentration to mimic healthy, and CF pathophysiology and biophysical properties were evaluated with macro- and microrheology. Biofilms were also characterized after exposure to DNase or DTT to examine the effects of DNA and mucin degradation, respectively. Identifying critical targets in biofilms for disrupting mechanical stability in highly concentrated mucus may lead to the development of efficacious biofilm therapies and ultimately improve CF patient outcomes. Overall mucus concentration was the predominant contributor to biofilm viscoelasticity and both DNA degradation and mucin reduction resulted in compromised biofilm mechanical strength.

**IMPORTANCE** Pathological mucus in cystic fibrosis (CF) is highly concentrated and insufficiently cleared from the airway, causing chronic inflammation and infection. *Pseudomonas aeruginosa* establishes chronic infection in the form of biofilms within mucus, and this study determined that biofilms formed in more concentrated mucus were more robust and less susceptible to mechanical and chemical challenges compared to biofilms grown in lower concentrated mucus. Neither DNA degradation nor disulfide bond reduction was sufficient to fully degrade biofilms. Mucus rehydration should remain a priority for treating CF pulmonary disease with concomitant multi-mechanistic biofilm degradation agents and antibiotics to clear chronic infection.

**KEYWORDS** *Pseudomonas aeruginosa*, biofilm, cystic fibrosis, mucins, DNA

Chronic respiratory infection by *Pseudomonas aeruginosa* is a major contributor to morbidity and mortality in cystic fibrosis (CF) (1–3). The CF airway is characterized by abnormal mucus properties, including hyperconcentration, increased viscoelasticity, and decreased mucociliary transport (4–6). Mucins, high molecular weight glycoproteins, form a polymeric mesh network that is responsible for the viscoelastic properties of mucus (4, 7). Abnormal water absorption, mucus dehydration, and mucin hypersecretion in CF together result in highly concentrated mucus in the airway which promotes chronic respiratory infections (5, 8). Mucus in CF represents an ideal growth environment for *P. aeruginosa* as it both provides a physical mesh to grow within and acts as a nutrient source (5, 9). High density gels such as >0.6% agarose and CF sputum promote bacterial aggregation (8), and attachment to mucins has been
hypothesized to improve biofilm stability (5, 8, 10). Indeed, pathological mucus properties are associated with increased incidence of infection, and P. aeruginosa in particular establishes biofilms, which are viscoelastic aggregates of bacteria protected by a matrix of extracellular polymeric substances (EPS) (5, 11, 12). The composition of biofilm EPS is dependent upon a number of factors, including the biophysical and biochemical properties of the growth environment (13–15).

Both mucus and biofilms have viscoelastic properties that are heavily influenced by the concentration and composition of polymeric substances (4, 11). For mucus, those polymers include DNA, which is released into the airway as a result of the chronic inflammatory response and mucins (16, 17). In biofilms, the EPS include DNA that bacteria self-produce or uptake from the environment, polysaccharides, lipids, and proteins (13). The importance of DNA in both mucus and biofilm biophysical properties has recently been investigated and correlated with decreased transport of mucus (17) and antibiotic susceptibility in biofilms (2, 18). In biofilms, extracellular DNA (eDNA) is increased when DNA concentrations in the environment are increased, and eDNA has been associated with increased biofilm viscoelasticity and decreased susceptibility to mechanical and chemical challenge (2, 18, 19). However, the role of DNA in airway mucus in influencing biofilm biophysical properties has yet to be elucidated.

In general, the relationship between airway mucus composition and biofilm recalcitrance is poorly understood. It has been established independently that increased mucus concentration promotes biofilm formation (5, 8) and that increased eDNA concentrations are associated with more robust biofilms (2, 18, 19), but biofilm mechanical properties as a function of DNA concentrations in mucus have not yet been evaluated. It is essential to understand how changes in mucus composition and concentration affect biofilm mechanics and susceptibility in order to identify potential therapeutic targets and improve patient outcomes. Conventional antibiotics are limited by poor diffusion through and reduced efficacy in mucus (20, 21). Additionally, the rise in antibiotic resistance limits the spectrum of antibiotics available to use for chronic infections, particularly as biofilms inherently exhibit decreased susceptibility to antibiotics compared with their planktonic counterparts (22, 23). Improving our understanding of biofilm mechanics will ultimately lead to more effective treatment design.

Herein, we describe the evaluation of P. aeruginosa biofilm mechanical strength with macro- and microrheological techniques as a function of human bronchial epithelial (HBE) mucus composition. Mucus at 2% and 5% solids to represent healthy and pathological mucus, respectively, was supplemented with salmon sperm DNA at 100:1 and 20:1 mucin to DNA ratios to mimic early and more advanced CF mucus (17, 24). Biofilms were also exposed to the DNA degradation enzyme, DNase, or to a reducing agent, dithiothreitol (DTT), to investigate: (i) the relative contribution of DNA in mucus to biofilm mechanical strength, and (ii) the disruption of chemical bonds and physical interactions in the biofilm matrix. Identifying key targets for biofilm disruption as a function of mucus composition may improve the selection and efficacy of future antibiofilm treatments in CF pulmonary disease.

RESULTS

The combination of mucins and DNA produce mechanically strong biofilms in nutrient broth. To first evaluate the individual contributions of mucins and DNA in the growth media to biofilm mechanical strength, P. aeruginosa biofilms were grown in tryptic soy broth (TSB) supplemented with porcine gastric mucins (PGM) which has a reported molecular mass of 4,000 to 5,000 kDa (Sigma M1778) and/or salmon sperm DNA which has a reported molecular mass of 2 kbp (Sigma D1626) at concentrations used for making artificial sputum media (ASM). This reductionist approach was taken first to determine if environmental mucins or DNA in the growth media individually contribute to biofilm mechanical properties or if the combination of the two is necessary for robust biofilm formation. The concentrations of PGM or DNA used was 5 mg/mL, which has traditionally been used for preparing ASM (18, 25), and a 10-fold dilution to investigate concentration effects. Healthy mucus contains ~1 mg/mL mucins and ~10 μg/mL DNA.
DNA (26, 27) while pathological mucus has mucin concentrations of >5 mg/mL and DNA concentrations of >100 μg/mL (4, 16, 28). Thus, this range of mucin and DNA concentrations spans the spectrum of health and disease. Combinations of PGM and DNA were made with PGM at 5 mg/mL and mucin to DNA ratios of 100:1 (i.e., 0.05 mg/mL DNA) and 20:1 (i.e., 0.25 mg/mL DNA) to mimic mucin to DNA ratios observed in CF in preschool aged children and adults, respectively (17). The investigation of biofilm growth in nutrient-rich broth (TSB), with the addition of PGM and DNA alone and in combination, enables the analysis of the relative contributions of PGM–DNA interactions to the biophysical properties of biofilms. Pseudomonas aeruginosa biofilms exhibited viscoelasticity with an elastic modulus (G’) greater than the viscous modulus (G’’), meaning they behave as a soft viscoelastic solid, i.e., tanδ < 0.5 (29). The addition of DNA alone to TSB had no significant effect (P > 0.05) on biofilm macrorheology, regardless of DNA concentration (Table 1). In contrast, the addition of PGM alone to TSB resulted in significantly (P < 0.05) decreased complex viscosity (η*, 0.05 Pa-s) of biofilms compared with TSB alone (0.10 Pa-s). A similar phenomenon has been described previously where low concentrations of mucins have been shown to prevent biofilm formation (30–32). The combinations of PGM and DNA in media resulted in mechanically stronger biofilms compared with TSB alone, with η* values being 3 to 4 times greater. Both mucin to DNA ratios of 100:1 and 20:1 produced biofilms with statistically similar η* values, 0.31 and 0.41 Pa-s, respectively, though the larger DNA concentration (20:1) was associated with a greater absolute value of η*. Viscometry analysis of the growth media show slight increases in macroscopic media viscosity with the addition of PGM and DNA, particularly at 20:1 mucins to DNA, but particle tracking microrheology (PTMR) indicates that all growth media behave as water (Fig. 1).

To elucidate the importance of eDNA in biofilm mechanical stability, biofilms were grown in TSB alone, exposed to the DNA degradation enzyme, DNase, and evaluated with PTMR. Microrheology is capable of resolving spatial heterogeneity that is lost in the bulk measurement of macrorheology (33). The degradation of eDNA within the biofilm was hypothesized to compromise structural integrity. Exposing TSB biofilms to DNase resulted in significant changes in biofilm microrheology (Fig. 2), including mean η* and heterogeneity, as demonstrated by the swarm charts in Fig. 2A. Quantification of heterogeneity was performed using the non-Gaussian parameter, κ, wherein greater κ values indicate more heterogeneity within the sample (34). For normal Brownian motion, the value of κ should be ≪1 (34). Values of κ for each DNase concentration are listed in Fig. 2A. The most homogeneous sample was biofilms treated with 100 μg/mL DNase, though all doses of DNase were associated with decreased κ values. The lowest tested dose, 10 μg/mL, had no significant effect on biofilm complex viscosity, η* (Fig. 2B), but 20 μg/mL increased η*. The greatest doses of DNase, 100 and 150 μg/mL, resulted in η* values greater than that of the PBS-treated control but lower than that for 20 μg/mL DNase. No tested concentration of DNase reduced biofilm η* to that of water (1 mPa-s), indicated by the dashed line in Fig. 2C. Thus, greater concentrations of DNase may be needed to fully dissociate the biofilm.

| TABLE 1 | Macroscopic moduli of P. aeruginosa biofilms grown in TSB as a function of mucin and DNA concentrations* |
|-----------------------------------------------|
| Growth media | G’ (Pa) | G” (Pa) | η* (Pa-s) |
|----------------|--------|--------|-----------|
| TSB            | 0.64 ± 0.27 | 0.11 ± 0.03 | 0.10 ± 0.04 |
| DNA 0.5 mg/mL  | 0.78 ± 0.43 | 0.18 ± 0.08b | 0.13 ± 0.07 |
| DNA 5 mg/mL    | 0.78 ± 0.52 | 0.18 ± 0.12 | 0.14 ± 0.09 |
| PGM 0.5 mg/mL  | 0.21 ± 0.11b | 0.06 ± 0.02 | 0.04 ± 0.02b |
| PGM 5 mg/mL    | 0.33 ± 0.15b | 0.07 ± 0.03 | 0.05 ± 0.02b |
| PGM:DNA 100:1  | 1.86 ± 1.40b | 0.47 ± 0.32b | 0.31 ± 0.23b |
| PGM:DNA 20:1   | 2.50 ± 0.49b | 0.71 ± 0.34b | 0.41 ± 0.25b |

*Data are presented as the mean and standard deviation of ≥3 separately grown and analyzed biofilms.  
bP < 0.05 compared with TSB biofilms.  
cPGM held at 5 mg/mL and DNA adjusted to ratio.

mSphere
Increasing overall mucus concentration and DNA to mucin ratios resulted in increased viscoelasticity. To more accurately mimic CF physiology, mucus collected from human bronchial epithelial (HBE) cultures was selected as a biofilm growth media. (28, 35) First, the biophysical properties of mucus were evaluated as a function of salmon sperm DNA concentrations to determine the effect of DNA on mucus viscoelasticity. A comparison of the macro and micro rheology of 2% and 5% mucus demonstrated that more concentrated mucus exhibited greater viscoelastic moduli (Table 2), in keeping with previous work (5, 16). On the macro scale, the complex viscosity (η*)

**FIG 1** Rheology of TSB growth media with PGM (5 mg/mL) and DNA at 100:1 and 20:1 mucin to DNA ratios. Right panel: macroscopic viscometry analysis of media types. Data are presented as mean ± standard deviation of ≥3 measurements. Left panel: microscopic complex viscosity of media types. Data are presented as kernel density estimate of probability density function for all tracked beads (n > 50).

**FIG 2** Biofilms grown in TSB micro rheology as a function of DNase concentration. (A) Swarm chart of all tracked bead η* measurements in treated biofilms with k values listen in table above corresponding dose of DNase. (B) Mean ensemble η* and standard deviation of treated biofilms. (C) Probability distribution of each bead η* for each condition. The viscosity of water is indicated by the dashed line. Data are presented for all beads tracked in ≥3 separately grown and analyzed biofilms. Statistical analysis with the Anderson-Darling test determined that all treatments of DNase were significantly (P < 0.05) different from PBS treatment.
of 5% mucus was greater than that of 2% by a factor of ~3. The addition of DNA did not significantly increase $\eta^*$ in 2% mucus but macroscopic moduli were significantly greater in 5% mucus with DNA. Both $G'$ and $G''$ values trended with $\eta^*$ and were significantly increased in 5% mucus with DNA. Particle tracking microrheology showed that $\eta^*$ was greater in mucus with DNA at both 2% and 5% (Fig. 3), though the most significant contributor to $\eta^*$ was overall concentration. In addition, 2% mucus was characterized by a bimodal distribution of lower $\eta^*$, more water-like component and a higher $\eta^*$, more solid-like component (Fig. 3A), in agreement with previous work (28). This bimodality was likewise observed in 2% mucus with DNA supplementation, suggesting that the addition of DNA at these concentrations is insufficient to homogenize mucus $\eta^*$ values into a single peak that is observed in greater concentrations of HBE mucus (4). Statistical analysis of PTM data with the Anderson-Darling test confirms that mucus at

| Mucus          | $G'$ (Pa)         | $G''$ (Pa)  | $\eta^*$ (Pa s) |
|---------------|------------------|-------------|-----------------|
| 2% HBE        | 0.465 ± 0.200    | 0.227 ± 0.039 | 0.082 ± 0.031   |
| 2% 100:1      | 0.523 ± 0.343    | 0.195 ± 0.077 | 0.090 ± 0.055   |
| 2% 20:1       | 0.464 ± 0.346    | 0.173 ± 0.101$^b$ | 0.079 ± 0.057   |
| 5% HBE        | 0.838 ± 0.354    | 0.451 ± 0.074 | 0.153 ± 0.055   |
| 5% 100:1      | 1.782 ± 0.642$^a$ | 1.055 ± 0.494$^b$ | 0.330 ± 0.128$^b$ |
| 5% 20:1       | 1.986 ± 0.823$^a$ | 1.586 ± 0.174$^b$ | 0.418 ± 0.083$^b$ |

aData are presented as the mean and standard deviation of ≥3 separately prepared and analyzed mucus samples.

$^aP < 0.05$ compared with same concentration mucus without DNA.

FIG 3  Mucus microrheology as a function of concentration and composition. Swarm chart of all tracked bead $\eta^*$ measurements in each mucus type. The non-Gaussian parameter $\kappa$ is listed above each mucus type. (B) Mean ensemble $\eta^*$ and standard deviation for each mucus type. (C) Probability distribution of each bead $\eta^*$ for each condition. The viscosity of water is indicated by the dashed line. Data are presented as the distribution of all tracked beads in ≥3 separately prepared and analyzed samples.
DTT caused an increase in biofilm concentration-dependent manner (Table 6). Some concentrations of DNase or agents. Reductions in biofilm concentration in comparison with DNase is critical for the design of novel efficacious antibiofilms. While DTT is cytotoxic (36, 37), evaluation of the efficacy of a reducing agent against in vitro biofilms in comparison with DNase is critical for the design of novel efficacious antibiofilm agents. Reductions in biofilm macro rheology by DNase or DTT occurred in a predominantly concentration-dependent manner (Table 6). Some concentrations of DNase or DTT caused an increase in biofilm η*, but this phenomenon was not consistent across mucus compositions. For example, 5% HBE biofilm η* increased at 10 μg/mL DNase but was indistinguishable at 100 and 1,000 μg/mL. However, DTT reduced 5% HBE biofilm η* at 15 and 150 μg/mL but increased biofilm η* at 1,500 μg/mL. Degradation of DNA concentration in both 2% and 5% mucus was nonsignificant (Table 3).

### Biofilm rheology is correlated with mucus rheology

After mucus characterization, *P. aeruginosa* biofilms were grown in HBE mucus at 2% and 5% total solids with no DNA, 100:1 mucin to DNA, or 20:1 DNA. Biofilms grown in mucus were rheologically similar to those grown in nutrient broth (Tables 1 and 4). All biofilms were dominated by G’ (tanδ < 0.5) similar to mucus. The presence of DNA in mucus was not associated with any significant changes in macroscopic moduli (Table 4). The predominant discriminator between biofilm rheology was overall mucus concentration, with 5% mucus types facilitating the growth of more robust biofilms (i.e., greater G’, G*" and η* values). The same trend was observed with PTMR wherein biofilms grown in 5% mucus types exhibited one peak at a greater mean η* compared with those grown in 2% mucus types (Fig. 4). Consistent with mucus rheology (Fig. 3), biofilms grown in 2% mucus types also demonstrated a bimodal distribution into distinct lower and greater η* groupings (Fig. 4A). The addition of DNA to 5% mucus was correlated with a greater mean biofilm η*, and biofilms were more heterogeneous compared to those grown in the absence of DNA. Biofilms grown in 5% mucus had significantly (P < 0.05) greater macroscopic moduli compared with those grown in 2% mucus, but no differences were measured with the addition of DNA at any tested concentration. Statistical analysis of PTMR data confirmed that biofilms grown in 5% mucus were significantly (P < 0.05) different from those grown in 2% mucus (Table 5). The difference between DNA concentrations in 5% mucus was nonsignificant (Table 5), suggesting that mucus concentration was the dominant factor.

### Treatment with DNase or DTT affects biofilm rheology

Biofilms were treated with DNase to degrade eDNA or with DTT, a powerful reducing agent. While DTT is cytotoxic (36, 37), evaluation of the efficacy of a reducing agent against in vitro biofilms in comparison with DNase is critical for the design of novel efficacious antibiofilm agents. Reductions in biofilm macro rheology by DNase or DTT occurred in a predominantly concentration-dependent manner (Table 6). Some concentrations of DNase or DTT caused an increase in biofilm η*, but this phenomenon was not consistent across mucus compositions. For example, 5% HBE biofilm η* increased at 10 μg/mL DNase but was indistinguishable at 100 and 1,000 μg/mL. However, DTT reduced 5% HBE biofilm η* at 15 and 150 μg/mL but increased biofilm η* at 1,500 μg/mL. Degradation of

### Table 3: Statistical analysis of mucus microrheology as a functional of concentration and composition

| P value | 2% HBE | 2% HBE 100:1 | 2% HBE 20:1 | 5% HBE | 5% HBE 100:1 |
|---------|--------|--------------|-------------|--------|--------------|
| 2% HBE 100:1 | 2.34E-204 | 2.34E-204 | 2.34E-204 | 2.34E-204 | 2.34E-204 |
| 2% HBE 20:1 | 1.29E-202 | 1.27E-202 | 1.25E-202 | 1.23E-202 | 1.21E-202 |
| 5% HBE | 0.96E-198 | 0.94E-198 | 0.92E-198 | 0.90E-198 | 0.88E-198 |
| 5% HBE 100:1 | 3.61E-108 | 3.59E-108 | 3.57E-108 | 3.55E-108 | 3.53E-108 |
| 5% HBE 20:1 | 1.06E-71 | 1.04E-71 | 1.02E-71 | 1.00E-71 | 0.98E-71 |

*Complex viscosity values were evaluated at 1 Hz using the Anderson-Darling test.

*Values that are > 0.05 are bolded for clarity.

### Table 4: Biofilm macroscopic moduli as a function of mucus concentration and composition

| Biofilm | G’ (Pa) | G*" (Pa) | η* (Pa-s) |
|---------|--------|----------|----------|
| 2% HBE | 0.477 ± 0.401 | 0.166 ± 0.123 | 0.081 ± 0.066 |
| 2% 100:1 | 0.758 ± 0.314 | 0.250 ± 0.082 | 0.127 ± 0.051 |
| 2% 20:1 | 0.667 ± 0.567 | 0.217 ± 0.140 | 0.112 ± 0.092 |
| 5% HBE | 1.762 ± 0.856 | 0.714 ± 0.367 | 0.303 ± 0.147 |
| 5% 100:1 | 1.618 ± 1.055 | 0.624 ± 0.365 | 0.276 ± 0.178 |
| 5% 20:1 | 1.369 ± 0.144 | 0.566 ± 0.054 | 0.236 ± 0.022 |

*Data are presented as the mean and standard deviation of ≥ 3 separately grown and analyzed biofilms. 5% HBE type biofilms were significantly different (P < 0.05) from 2% HBE type biofilms, but no significance observed between biofilms grown with the same mucus concentration.
the biofilm extracellular matrix allows for the disruption and release of interior components such as both live and dead bacterial cells exoenzymes, swellable polysaccharides, proteins, and lipids (13), which can increase bulk rheology. Indeed, biofilm disruption and bacterial cell death via nitric oxide or tobramycin exposure has previously been shown to increase biofilm macrorheology (18). The use of PTMR improves the analysis of local viscosity in the biofilm and describes biofilm heterogeneity (Fig. 5 and 6). Biofilms grown in all 2% HBE mucus types were similarly affected by mid (150 μg/mL) to high (1,500 μg/mL) doses of DTT (Fig. 5). The higher h* component of 2% biofilms disappeared with DTT treatment. Uniquely, the largest dose of DTT reduced 5% biofilm mean h* and was associated with a second peak at lower h* (Fig. 6), similar to untreated 2% biofilms. This effect was also observed at the largest dose of DNase.

![FIG 4](image-url)

**FIG 4** Biofilm micro rheology as a function of mucus concentration and composition. (A) Swarm chart of all tracked bead $\eta^*$ measurements in biofilms. The non-Gaussian parameter $\kappa$ is listed above each biofilm. Dashed line represents the viscosity of water. (B) Mean ensemble $\eta^*$ and standard deviation of biofilms. (C) Probability distribution of each bead $\eta^*$ for each condition. The viscosity of water is indicated by the dashed line. Data are presented for all beads tracked in ≥3 separately grown and analyzed biofilms.

| $P$ value | PAO1 2% | PAO1 2% 100:1 | PAO1 2% 20:1 | PAO1 5% | PAO1 5% 100:1 |
|-----------|---------|---------------|--------------|---------|---------------|
| PAO1 2% 100:1 | 2.57E-04 | 1.36E-05 | 6.25E-127 | 1.18E-101 | 4.66E-103 |
| PAO1 2% 20:1 | 5.18E-10 | 2.26E-145 | 2.67E-111 | 3.97E-111 | 7.44E-15 |
| PAO1 5% | 1.00E-85 | 9.39E-14 | 6.67E-111 | 5.72E-111 | 9.39E-15 |
| PAO1 5% 100:1 | 2.26E-145 | 7.44E-15 | 3.97E-111 | 7.44E-15 | 0.9289* |

| $P$ value | PAO1 5% 20:1 | PAO1 5% 20:1 |
|-----------|-------------|-------------|
| PAO1 5% | 1.18E-101 | 4.66E-103 |
| PAO1 5% 100:1 | 2.46E-71 | 9.52E-73 |
| PAO1 5% 20:1 | 6.67E-111 | 3.97E-111 |

*Complex viscosity values were evaluated at 1 Hz using the Anderson-Darling test.

bValues that are >0.05 are bolded for clarity.
Indeed, the effects of high dose DNase were apparent in histograms of $\eta^*$ in Fig. 7. Untreated 2% biofilms had a distinct bimodal distribution into low and high viscosity components. Treatment with DNase reduced the proportion of signal in the higher $\eta^*$ component, shifted the absolute mean $\eta^*$ value down closer to water, and increased the relative proportion of the low $\eta^*$ component. Biofilms grown in 2% 20:1 also included a component with the viscosity of water after exposure to DNase, indicated by the dashed line. Biofilms grown in 5% mucus types have a single peak with PBS treatment, but upon exposure to DNase, a lower $\eta^*$ component appears in the histogram. Mean and standard deviation data of PTMR experiments quantifying the efficacy of treatments on biofilm rheology are given in Table 7.

**DISCUSSION**

This study represents the first examination into the relationship between mucus concentration/composition and *P. aeruginosa* biofilm mechanical properties. The contributions of mucus concentration and composition to biofilm strength are critical to understand due to the increasing concentration of mucins and DNA with CF pulmonary disease progression. We hypothesized that the viscoelastic properties of *Pseudomonas aeruginosa* biofilms grown in mucus would be dominated by the overall mucus concentration and composition, similar to mucus (4, 16, 17). Indeed, *P. aeruginosa* biofilms grown in nutrient broth (TSB) behaved as a viscoelastic solid ($\tan\delta <0.5$), with $G'$ greater than $G^*$ at 0.64 and 0.11 Pa, respectively (Table 1). Regardless of media composition (i.e., with or without mucins and DNA), all *P. aeruginosa* biofilms studied behaved as viscoelastic solids, likely due to the prevalence of strong chemical and physical interactions in the extracellular matrix between polymers such as eDNA and polysaccharides. Consistent with previous reports (30–32), low concentrations of PGM (0.5 and 5 mg/mL) in TSB inhibited robust biofilm formation, as $G'$ was about half that of those grown in TSB alone. In contrast, DNA in the growth media alone did not significantly affect biofilm rheology, neither at 0.5 nor 5 mg/mL. However, the combination of PGM and DNA in TSB facilitated robust biofilm formation with macrorheology values 3 to 4 times greater than those grown in TSB alone (Table 1). Thus, the combination of mucins and DNA in media are associated with mechanically robust biofilms while the individual polymers are not.

Biofilms utilize both endogenously produced and environmentally derived DNA for mechanical stability (18). Treatment with DNase, the DNA degradation enzyme, enzymatically cleaves eDNA in biofilm and alters viscoelastic properties. While the lowest dose of DNase tested by microrheology, 10 $\mu$g/mL, had no significant impact on $\eta^*$, 20 $\mu$g/mL increased $\eta^*$ compared with the PBS-treated control. By degrading eDNA in the matrix, chemical bonds are broken, interactions are disrupted, and biofilm components (e.g., cells, biomacromolecules) are released from the interior. Biofilm heterogeneity ($\chi$) increased and EPS rearrangement due to minimal eDNA degradation likely contributed to greater $\eta^*$. Biofilm $\eta^*$ was greater compared with the PBS-treated control but decreased compared with biofilms exposed to 20 $\mu$g/mL DNase, suggesting a threshold concentration for uniform biofilm degradation for these biofilms. Biofilm heterogeneity is of significant concern when treating with antibiotics due to the risk of fostering antibiotic resistance when the biofilm is not completely eradicated (3, 38);

**TABLE 6** Biofilm macroscopic $\eta^*$ after 24 h exposure to DNase or DTT

| Treatment     | 2% HBE  | 2% 100:1 | 2% 20:1 | 5% HBE  | 5% 100:1 | 5% 20:1 |
|---------------|---------|----------|---------|---------|----------|---------|
| PBS           | 0.081 ± 0.066 | 0.127 ± 0.051 | 0.112 ± 0.092 | 0.303 ± 0.147 | 0.276 ± 0.178 | 0.236 ± 0.022 |
| DNase 10 ug/mL| 0.005 ± 0.003 | 0.046 ± 0.009 | 0.096 ± 0.007 | 1.700 ± 0.148 | 0.196 ± 0.036 | 0.475 ± 0.054 |
| DNase 100 ug/mL| 0.009 ± 0.004 | 0.052 ± 0.009 | 0.018 ± 0.004 | 0.250 ± 0.024 | 1.243 ± 0.116 | 0.591 ± 0.045 |
| DNase 1,000 ug/mL| 0.211 ± 0.020 | 0.026 ± 0.004 | 0.012 ± 0.003 | 0.292 ± 0.033 | 0.153 ± 0.033 | 0.110 ± 0.003 |
| DTT 15 ug/mL  | 0.030 ± 0.004 | 0.130 ± 0.081 | 1.337 ± 0.629 | 0.105 ± 0.003 | 0.122 ± 0.009 | 0.292 ± 0.012 |
| DTT 150 ug/mL | 0.202 ± 0.018 | 0.048 ± 0.010 | 0.025 ± 0.006 | 0.147 ± 0.006 | 0.138 ± 0.007 | 0.207 ± 0.008 |
| DTT 1,500 ug/mL| 0.477 ± 0.068 | 0.049 ± 0.012 | 0.059 ± 0.036 | 0.477 ± 0.068 | 0.085 ± 0.002 | 0.158 ± 0.004 |

*Data are presented as the mean and standard deviation of $n=3$ separately grown and treated biofilms.*
thus, the non-Gaussian parameter of treated biofilms may serve as a quantitative measure of biofilm homogenization. Complete biofilm degradation to the viscosity of water was not achieved with any tested dose of DNase, which indicates that greater concentrations may be necessary or that DNA degradation alone is insufficient to fully degrade biofilms. Combinations of antibiotics and DNase have previously been investigated for superior biofilm eradication (39) and future work will investigate these combinations in mucus-grown biofilms.

The presence of both mucins and DNA together in growth media promotes robust biofilm development, and targeting eDNA in the biofilm matrix allows for partial biofilm degradation. HBE mucus was then used as a growth medium for *P. aeruginosa* biofilms using salmon sperm DNA at physiologically relevant mucin to DNA ratios (17, 24). First, the viscoelastic properties of mucus as a function of concentration and composition were evaluated, and more concentrated mucus was characterized by greater viscoelastic moduli, with 5% being 2 to 3 times greater than 2% (Table 2). The addition of DNA to mucus also increased $G'$, $G''$, and $\eta^*$. While the absolute values of 5% mucus

**FIG 5** Biofilms grow in 2% HBE microrheology after 24 h exposure to DNase or DTT treatment (\(\mu\)g/mL). Data are presented as a swarm chart of all tracked bead $\eta^*$ in $\geq 3$ separately grown and treated biofilms.
η* trended with DNA concentration, both 5% 100:1 and 5% 20:1 mucus were statistically indistinguishable from 5% mucus without DNA on the macrorheological scale. Mucus physical properties was further resolved with PTMR (Fig. 2) where 2% mucus exhibited the bimodal behavior characteristic of healthy mucus. The bimodal behavior was mirrored in 2% 100:1 and 2% 20:1, though the curves shifted to greater η*. The prevalence of the lower η* peak (more water-like) was also reduced in mucus with DNA, indicating that 2% mucus with DNA was dominated by the greater η*, or more solid-like, component. Previous work demonstrated that concentrated CF mucus facilitated biofilm formation while 2% mucus did not (5), suggesting the need for a sufficiently robust viscoelastic behavior (i.e., threshold G', G″ or η* values) in order to allow biofilms to form in mucus.

Indeed, _P. aeruginosa_ biofilms grown in 5% were characterized by greater viscoelastic moduli than biofilms grown in 2% by about 4 times. Uniquely, biofilms grown in all 2% mucus types exhibited nearly uniform bimodal distribution into lower and

**FIG 6** Biofilms grow in 5% HBE microrheology after 24 h exposure to DNase or DTT (μg/mL) treatment. Data are presented as a swarm chart of all tracked bead η* in ≥3 separately grown and treated biofilms.
higher $\eta^*$ components (Fig. 4). However, similar to mucus, the greatest contributor to biofilm rheology was overall mucus concentration (Fig. 3 and 4). Significant ($P < 0.05$) increases in macroscopic and microscopic moduli were observed between 2% and 5% mucus and in biofilms grown therein. The addition of DNA to mucus was not associated with any significant changes in macroscopic moduli compared with biofilms without DNA. Thus, while DNA is essential to biofilm mechanical stability, the presence of DNA in mucus does not significantly impact the structural integrity of these $P. aeruginosa$ biofilms. In fact, only overall mucus concentration was observed to affect biofilm macroscopic and microscopic moduli.

Biofilms were exposed to DNase to degrade the eDNA in the matrix or to DTT, which is a reducing agent. Both agents degrade biomolecules in the extracellular matrix and disrupt interactions. For simplicity, only biofilm $\eta^*$ will be discussed here. In biofilms grown in 2% mucus $\pm$ DNA, DNase at 100 $\mu$g/mL consistently reduced macroscopic biofilm $\eta^*$ (Table 6). However, at 1,000 $\mu$g/mL DNase, the $\eta^*$ of 2% HBE biofilms more than doubled. Biofilms grown in 2% mucus supplemented with DNA were characterized by decreased $\eta^*$ after exposure to 1,000 $\mu$g/mL DNase (Table 4) at both 100:1 and 20:1 mucin to DNA ratios. The increase in biofilm $\eta^*$ is likely due to cell lysis and the release of cells and stiff cellular debris that results in a greater measured bulk

### Table 7 Biofilm $\eta^*$ measured via PTMR after 24 h exposure to DNase or DTT

| Treatment   | PAO1 2% HBE | PAO1 2% 100:1 | PAO1 2% 20:1 | PAO1 5% HBE | PAO1 5% 100:1 | PAO1 5% 20:1 |
|-------------|-------------|---------------|--------------|-------------|---------------|--------------|
| PBS         | 0.050 ± 0.033 | 0.058 ± 0.041 | 0.034 ± 0.022 | 0.224 ± 0.039 | 0.355 ± 0.018 | 0.356 ± 0.122 |
| DNase 10 $\mu$g/mL | 0.026 ± 0.019 | 0.072 ± 0.029 | 0.027 ± 0.020 | 0.153 ± 0.033 | 0.139 ± 0.027 | 0.260 ± 0.064 |
| DNase 100 $\mu$g/mL | 0.004 ± 0.000 | 0.064 ± 0.023 | 0.025 ± 0.014 | 0.154 ± 0.046 | 0.464 ± 0.175 | 0.199 ± 0.062 |
| DNase 1,000 $\mu$g/mL | 0.004 ± 0.001 | 0.020 ± 0.011 | 0.015 ± 0.010 | 0.232 ± 0.070 | 0.107 ± 0.033 | 0.114 ± 0.033 |
| DTT 15 $\mu$g/mL   | 0.009 ± 0.002 | 0.009 ± 0.001 | 0.028 ± 0.016 | 0.106 ± 0.023 | 0.140 ± 0.036 | 0.199 ± 0.064 |
| DTT 150 $\mu$g/mL  | 0.005 ± 0.000 | 0.007 ± 0.001 | 0.023 ± 0.015 | 0.274 ± 0.091 | 0.134 ± 0.035 | 0.146 ± 0.047 |
| DTT 1,500 $\mu$g/mL | 0.027 ± 0.019 | 0.009 ± 0.002 | 0.007 ± 0.000 | 0.472 ± 0.119 | 0.213 ± 0.105 | 0.132 ± 0.050 |

*Data are presented as the mean and standard deviation of all tracked beads in $\geq 3$ separately grown and treated biofilms.
chronic respiratory infections. Regardless of the DNA concentration in mucus, the concentration of airway mucus in CF patients may help prevent the establishment of mucus viscoelasticity but not necessarily increased biofilm mechanical strength. Decreasing the concentration of DNA in mucus was greater, DNase degraded eDNA and decreased bulk biofilm $\eta^*$ at 1,000 $\mu$g/mL DNase. All biofilms grown in 2% mucus types were similarly affected by 1,000 $\mu$g/mL DNase on the microrheology scale, with a decrease in the higher $\eta^*$ peak and an increase and/or shift of the lower $\eta^*$ peak (Fig. 5). Indeed, biofilms grown in 2% HBE with DNA at both concentrations were degraded by 1,000 $\mu$g/mL DNase and exhibited smaller macroscopic $\eta^*$. In contrast, biofilms grown in 2% HBE without DNA treated with 1,000 $\mu$g/mL DNase exhibited increased macroscopic $\eta^*$. We, therefore, posit that a threshold concentration of DNase is required to degrade eDNA without lysing bacterial cells, whereupon cellular components are released into the bulk and increase macroscopic viscoelasticity. A similar phenomenon was observed in biofilms grown in 5% mucus types. Macrorheological parameters increased with low (10 $\mu$g/mL) to medium (100 $\mu$g/mL) doses of DNase and decreased at 1,000 $\mu$g/mL (Table 4) while PTMR demonstrates a dose-dependent decrease in biofilm $\eta^*$ (Fig. 4 and 5).

While DTT physically disrupts P. aeruginosa biofilms, no consistent trend across mucus types was observed with DTT treatment, which reduces chemical bonds, including disulfide bonds. In 2% mucus biofilms, macroscopic moduli increased with DTT concentration (Table 6). The opposite effect was observed in 2% 100:1 biofilms. In 2% 20:1 biofilms, macroscopic $\eta^*$ dramatically increased with the lowest tested dose of DTT and then decreased below the value for the PBS-treated control with greater doses of DTT. The lack of an observable trend in biofilm macrorheology may be due in part to the toxicity of DTT, which generates reactive oxygen species (ROS) capable of damaging DNA (36, 37). Thus, any changes in biofilm rheology due to the reduction of chemical bonds (e.g., mucin disulfide bonds) in the extracellular matrix may be hidden by changes in rheology due to cell death and ROS reactions. Further, bulk rheology may be affected by cell lysis and the release of exoenzymes, swellable polysaccharides, proteins, and lipids as the biofilm is degraded (13, 18). Biofilm disruption with antibacterial agent treatment has previously been associated with increases in macroscopic moduli (18); thus, PTMR was used to evaluate changes in biofilm microrheology with DTT treatment. Microrheology of DTT-treated biofilms grown in 2% mucus types showed the presence of a tall and narrow peak at a $\eta^*$ near water (Fig. 5) suggesting that the physical biofilm had been sufficiently degraded for the 1-$\mu$m probe to measure a predominantly low $\eta^*$ fluid. In biofilms grown in 5% mucus types, DTT treatment was associated with an increase in biofilm heterogeneity and downward shift in $\eta^*$, suggestive of biofilm degradation. As macrorheology is dominated by the bulk rheological response, microrheology is consistently superior for investigating the biophysical effects of DNase and DTT treatment on P. aeruginosa biofilms. Together these data suggest that biofilm disruption alone is insufficient to consistently reduce biofilm $\eta^*$ to that of water, which would, in theory, contribute to improved clearance. Further work is needed to characterize the relationship between biofilm viscoelasticity and mucociliary clearance. Also, less cytotoxic reducing agents must be evaluated to better understand the impact of disulfide bond reduction between mucins in mucus-grown biofilms.

In summary, the predominant contributor to biofilm rheology was overall mucus concentration. The presence of DNA in mucus is associated with greater mucus viscoelasticity but not necessarily increased biofilm mechanical strength. Decreasing the concentration of airway mucus in CF patients may help prevent the establishment of chronic respiratory infections. Regardless of the DNA concentration in mucus, P. aeruginosa biofilm microrheology was reduced by DNase and DTT treatments, though bulk $\eta^*$ increased with biofilm disruption. Thus, treatments that target both eDNA and other EPS interactions may be superior antibiofilm agents for CF respiratory infection, though polymer degradation alone may be insufficient for biofilm eradication. Biofilm
mechanical strength has previously been associated with susceptibility to antibiotics (2, 11, 18). As both DNase and DTT are capable of physically degrading *P. aeruginosa* biofilms, their concomitant use with an antibacterial agent may facilitate superior biofilm eradication. Additionally, physical degradation of the biofilm may assist the host immune response in clearing the biofilm via phagocytosis or other clearance mechanisms. To prevent chronic infection, the modulation of mucus concentration will be critical. However, once chronic infection is established, physical biofilm disruption in combination with mucus hydration and mucolysis will promote eradication and clearance. Future work will investigate the combination of biofilm degradation and antibacterial action using antibacterial agents that are effective regardless of bacteria metabolism and evaluate mucociliary transport rates with treatment.

**MATERIALS AND METHODS**

**Materials.** All materials were used as received unless otherwise specified. Fluorescent 1 μm carboxylated latex beads (FluoSpheres, Invitrogen), TSB, tryptic soy agar (TSA), porcine gastric mucins (PGM, M1778), salmon sperm DNA (D1626), DNase, and DTT were purchased from Millipore Sigma. The *P. aeruginosa* strain PA01 was obtained from the American Type Culture Collection (Manassas, VA), ATCC #15692.

**Biofilm growth in nutrient broth and treatment.** TSB was inoculated with *P. aeruginosa* strain PA01 frozen stock and cultured overnight. The overnight culture was resuspended in fresh TSB and cultured at 37°C to an OD₆₀₀ of 0.25. Bacteria were further diluted in fresh TSB to a final concentration of 10⁶ CFU/mL, and 150 μL of this solution was added to the wells of a 96-well plate. The well plate was sealed with parafilm and incubated with shaking at 37°C for 3 days until a viscous macrocolony formed as previously described (40). TSB was also supplemented with porcine gastric mucins (PGM, 5 mg/mL) and salmon sperm DNA (4 mg/mL), either alone or in combination to match concentrations used in artificial sputum media (ASM) (41). The biofilm (50 μL) was removed from growth media and added to a microcentrifuge tube prior to treatment or analysis using a positive pressure pipette as previously described (18). Dissolved DNase in PBS was added in a volume of 5 μL or less into the center of the biofilm to final concentrations ranging from 10 to 1,000 μg/mL. Microcentrifuge tubes were incubated with shaking at 37°C for 24 h prior to analysis.

**Mucus preparation and biofilm growth.** Human airway epithelial cells were obtained by the Marsico Lung Institute Tissue Procurement and Cell Culture Facility and cultured at the air-liquid interface as previously described (16). Mucus washings were collected, pooled, and dialyzed. Total % solids was determined via dry weight calculations, and mucin content was quantified with refractometry. Mucus (100 μL) was added to a 96 well-plate and inoculated with *P. aeruginosa* to a final concentration of 10⁶ CFU/mL. For PTMR experiments, 2 μL of carboxylated latex beads at a 1:10 dilution from stock was added (18). Adjacent wells were filled with 200 μL distilled water to prevent evaporation, and the lid was sealed to the plate with parafilm. The sealed well plate was incubated with shaking at 37°C for 24 h until a visible, viscous macrocolony formed at the air-liquid interface as previously described (5, 9, 18, 42). The biofilm (50 μL) was removed from growth media and added to a microcentrifuge tube prior to treatment or analysis. Biofilms were treated with DNase or DTT in concentrations ranging from 10 to 1,500 μg/mL.

**Rheology.** Macrorheology was performed using a 20-mm 1° cone and plate rheometer and frequency sweeps as previously described (18). Particle tracking microrheology was performed with 1 μm carboxylated latex beads and video microscopy as previously described (18, 28). All measurements were repeated in biological duplicate with five technical replicates, and data are reported as the mean ± standard deviation. All values of frequency-dependent parameters are given as a single value from a frequency sweep assay with the value reported corresponding to the measured response at 1 Hz.

**Statistics.** Each measurement was repeated ≥3 times per sample. Mucus samples were separately prepared and analyzed. Biofilm samples were grown on different days using a fresh overnight solution. Data are presented as the mean and standard deviation. Statistical significance from macrorheology experiments was determined using a two-tailed Student’s *t* test. Statistical significance from PTMR experiments was determined using the Anderson-Darling test at 1 Hz.

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**REFERENCES**

1. Oliver A, Díez-Aguilar M, Köksal E, Ekkelenkamp M, Cantón R, Morosini MI. 2018. Use of Calgary and microfluidic biofilm systems to test the activity of fosfomycin and tobramycin alone and in combination against cystic fibrosis Pseudomonas aeruginosa biofilms. Antimicrob Agents Chemother 62:e01650-17. https://doi.org/10.1128/AAC.01650-17.

2. Rozenbaum RT, van der Mei HC, Woudstra W, de Jong ED, Busscher HJ, van der Mei HC, Woudstra W, de Jong D, Busscher HJ, Sharma PK. 2019. Role of viscoelasticity in bacterial killing by antimicrobials in differently grown *P. aeruginosa* biofilms. Antimicrob Agents Chemother 63:1–30. https://doi.org/10.1128/AAC.01972-18.
3. Fernández-Barat L, Cifou O, Kragh KN, Pressler T, Johansen U, Motos A, Torres A, Holby N. 2017. Phenotypic shift in Pseudomonas aeruginosa populations from cystic fibrosis lungs after 2-week antibiotic treatment. J Cyst Fibros 16:222–229. https://doi.org/10.1016/j.jcf.2016.08.005.

4. Hill DB, Long RF, Kissner WJ, Atieh E, Garbarine IC, Markovetz MR, Fontana NC, Christy M, Habibpour M, Tarran R, Forest MG, Boucher RC, Button B. 2014. Pathological mucus and impaired mucus clearance in cystic fibrosis patients result from increased concentration, not altered pH. Eur Respir J 52:1801297. https://doi.org/10.1183/13993003.01297-2014.

5. Matsui H, Wagner VE, Hill DB, Schwab UE, Rogers TD, Button B, Taylor RM, Superfine R, Rubinstein M, Igleswki BH, Boucher RC. 2006. A physical linkage between cystic fibrosis airway surface dehydration and Pseudomonas aeruginosa biofilms. Proc Natl Acad Sci USA 103:18131–18136. https://doi.org/10.1073/pnas.0604281103.

6. Boucher RC. 2019. Mucoid obstructive lung diseases. N Engl J Med 380:1941–1953. https://doi.org/10.1056/NEJMra1817999.

7. Lai SK, Wang Y-Y, Cone R, Wirtz D, Hanes J. 2009. Altering mucus rheology to “solidify” human mucus at the nanoscale. PLoS One 4:e4294. https://doi.org/10.1371/journal.pone.004294.

8. Staudinger BJ, Muller JF, Halldórsson S, Boles B, Angermeyer A, Nguyen D, Aguirre I, Pfeifer E, Bagg J, Langer K, Hill DB, Francoeur S, Kritchevsky ES, Frolov EI, Glicksman AC, Hill DB, Jugdutt BI, Hubalek M, Hanger M. 2017. Antibacterial nanocomplexes to protect and deliver drugs in biofilms in cystic fibrosis airways. J Cyst Fibros 16:222–229. https://doi.org/10.1016/j.jcf.2016.08.005.

9. Peterson BW, He Y, Ren Y, Zerdoum A, Libera MR, Sharma PK, van der Mei HC, Busscher HJ. 2015. Viscoelasticity of mucus in Pseudomonas aeruginosa biofilms. FEMS Microbiol Rev 39:234–255. https://doi.org/10.1111/1574-6974.12135.

10. Peterson BW, He Y, Ren Y, Zerdoum A, Libera MR, Sharma PK, van der Mei HC, Busscher HJ. 2015. Viscoelasticity of mucus and mucus functionally distinct exopolysaccharides. mBio 5:1–11. https://doi.org/10.1128/mBio.00136-14.

11. Fabbri S, Stoodley P. 2016. Mechanical properties of biofilms. Curr Opin Biotechnol 46:93–104. https://doi.org/10.1016/j.cub.2017.01.003.

12. Fabbri S, Stoodley P. 2016. Mechanical properties of biofilms. Curr Opin Biotechnol 46:93–104. https://doi.org/10.1016/j.cub.2017.01.003.

13. Co JY, Cárcamo-Oyarce G, Billings N, Wheeler KM, Grindy SC, Holten-Christensen KM, Krause DC, Radicioni G, Alexis NE, Kesimer M, Tiemeyer M, Boucher RC, Ehre C, Button B, Kesimer M, Ramsey KR. 2019. Mucin hyperconcentration in non–cystic fibrosis bronchiectasis. Am J Respir Cell Mol Biol 61:661–670. https://doi.org/10.1164/rccm.201906-1219OC.

14. Markovetz MR, Subramani DB, Kissner WJ, Morrison CB, Garbarine IC, Ghio A, Ramsey KA, Arora H, Kumar P, Nix DB, Kumagai T, Krukonys TM, Krause DC, Radicioni G, Alexis NE, Kesimer M, Tiemeyer M, Boucher RC, Ehre C, Button B. 2019. Endotracheal tube mucus as a source of airway mucus for rheological study. Am J Physiol Lung Cell Mol Physiol 317:L498–L509. https://doi.org/10.1152/ajplung.00238.2019.

15. pavlovsky L, Younger JG, Solomon MJ. 2013. In situ rheology of Staphylococcus epidermidis bacterial biofilms. Soft Matter 9:122–131. https://doi.org/10.1039/C2SM27005F.

16. Hill DB, Kruezek C, Naisar U, Colmer-Hamood JA, Hamood AN. 2014. Mucin inhibits Pseudomonas aeruginosa biofilm formation by significantly enhancing twitching motility. Can J Microbiol 60:155–166. https://doi.org/10.1139/cjm-2013-0570.

17. Co JY, Cáraddock-Oyarce G, Billings N, Wheeler KM, Grindy SC, Holten Andersen N, Ribbeck K. 2018. Mucins trigger dispersal of Pseudomonas aeruginosa biofilms. NPJ Biofilms Microbiomes 4:23. https://doi.org/10.1038/s41522-018-0067-0.

18. Caladara M, Friedlander RS, Kavaughna NL, Alzenberg J, Foster KR, Ribbeck K. 2012. Mucin biopolymers prevent bacterial aggregation by retaining cells in the free-swimming state. Curr Biol 22:2325–2330. https://doi.org/10.1016/j.cub.2012.10.028.

19. Lai SK, Hanes Y-Y, Wang Y-Y, Wirtz D, Hanes J. 2009. Micro- and macro-rheology of mucus. Adv Drug Deliv Rev 61:86–100. https://doi.org/10.1016/j.addr.2008.09.012.

20. Wagner CE, Turner BS, Rubinstein M, McKinley GH, Ribbeck K. 2017. A rheological study of the association and dynamics of MUC5AC gels. Biomacromolecules 18:3658–3664. https://doi.org/10.1021/acs.biomac.7b00809.

21. Kesimer M, Kirkham S, Pickles RJ, Henderson AG, Alexis NE, DeMaria G, Krause DC, Radicioni G, Ciofu O, Johansen HK, Song ZJ, Molin S, Jensen PØ, Molin S, Jensen PØ, Molin S. 2018. Persistence and microevolution of Pseudomonas aeruginosa in the cystic fibrosis lung: a single-patient longitudinal genomic study. Front Microbiol 9:3242. https://doi.org/10.3389/fmicb.2018.03242.

22. Winstanley C, O’Brien S, Brockhurst MA. 2016. Pseudomonas aeruginosa evolutionairy adaptation and diversification in cystic fibrosis chronic lung infections. Trends Microbiol 24:327–337. https://doi.org/10.1016/j.tim.2016.01.008.
39. Tetz GV, Artemenko NK, Tetz VV. 2009. Effect of DNase and antibiotics on biofilm characteristics. Antimicrob Agents Chemother 53:1204–1209. https://doi.org/10.1128/AAC.00471-08.

40. Rouillard KR, Novak OP, Pistiolis AM, Yang L, Ahonen MUR, McDonald RA, Schoenfisch MH. 2021. Exogenous nitric oxide improves antibiotic susceptibility in resistant bacteria. ACS Infect Dis 7:23–33. https://doi.org/10.1021/acsinfectdis.0c00337.

41. Sriramulu DD, Lünsdorf H, Lam JS, Römling U, Lünsdorf H, Lam JS, Romling U. 2005. Microcolony formation: a novel biofilm model of Pseudomonas aeruginosa for the cystic fibrosis lung. J Med Microbiol 54:667–676. https://doi.org/10.1099/jmm.0.45969-0.

42. Ahonen MJR, Dorrier JM, Schoenfisch MH. 2019. Antibiofilm efficacy of nitric oxide-releasing alginate against cystic fibrosis bacterial pathogens. ACS Infect Dis 5:1327–1335. https://doi.org/10.1021/acsinfectdis.9b00016.