Introduction

Breast cancer refers to cancer originating in the breast tissues, including the ducts and lobules [1]. According to the latest statistics published by the International Agency for Research on Cancer (IARC), breast cancer ranks as the second most commonly diagnosed cancer in the world. It also highlighted breast cancer as the most common cancer in females worldwide and is the first and second leading cause of all cancer-associated deaths in females in developing and developed regions, respectively [2]. Implementation of breast screening programmes have brought forward the lead time for detecting early breast cancer enabling improved treatment outcome [3]. For patients diagnosed with early-stage breast cancer, conservative management approach of breast-conserving surgery (BCS) is preferred over radical mastectomy commonly used in patients with late-stage breast cancer. The 13th St. Gallen International Breast Cancer Conference (2013) Expert Panel [4] however highlighted that unless post-operative radiation therapy could be delivered, BCS should be reconsidered. Addition of radiation therapy would help to reduce recurrence rates by eradicating the likely presence of microscopic disease after surgery [5]. Currently, radiation therapy presents as an integral component of early-stage, localised breast cancer treatment [5,6]. A large meta-analysis [7] found that radiation therapy delivered post-surgery resulted in ap-
parent reduction in the risk of local recurrences and mortality rate. In addition to improving the local and regional control, use of radiation therapy post-surgery for early-stage breast cancer treatment, also provided the advantage of maintaining patients’ quality of life (QOL) to a certain extent. This was attributed to the ability of keeping their breasts, thus maintaining their body image and femininity [6,8].

Radiation therapy is an integral component of early-stage breast cancer management and typically applied to the whole breast post-BCS [9]. Results obtained from randomized trials by the Early Breast Cancer Trialists’ Collaborative Group (EBCTCG) [7] revealed that whole breast radiation therapy (WBRT) post-BCS reduced rate of disease recurrence by half and mortality rate by a 6th for patients with early-stage breast cancer. Conventional approach of WBRT is with the use of three-dimensional conformal radiation therapy (3DCRT). However, this approach is associated with the challenge of achieving uniform target dose distribution [10] and introduction of undesired dose to the skin and adjacent organs, resulting in acute and long-term toxicities [6]. These issues stemmed from the steep breast contour change in the 3D shape of the breast and the proximity of target volume to critical organs and tissues. To address these challenges, advanced and complex radiation therapy technology have been developed over the years to increase target dose uniformity, reduce high-dose regions and doses to organs-at-risk (OARs). These are manifested in techniques such as intensity-modulated radiation therapy (IMRT), volumetric modulated arc therapy (VMAT), and electronic tissue compensation (Ecomp). However, there are trade-offs involved in these techniques in an attempt to improve the planning target volume (PTV) and OARs dosimetry. It was also documented in literature that several institutions and radiation therapy departments utilize varying treatment techniques and fractionation schedules for breast radiation treatments [11,12]. These differences could result in overall compromised quality of patient care, manpower, available resources and productivity of the department. Additionally, consensus on the optimal technique to be employed for WBRT is still lacking both in literature and clinically. There is also currently limited clinical implementation, research and data available on the use of other advanced techniques like Ecomp and Hybrid for WBRT compared to the other more commonly utilized techniques. Hence, the full extent of their effectiveness on breast cancer treatment remains only partially understood. Therefore, this study aims to: (1) assess the PTV dosimetry and determine the doses delivered to OARs for WBRT using the various treatment planning techniques; (2) evaluate and compare all the dosimetric parameters obtained for both PTV and OARs between the various techniques; and (3) identify an optimal technique that would be recommended for WBRT based on the comparison results.

Materials and Methods

1. Patient selection

This retrospective study utilized thirty anonymized planning computed tomography (CT) datasets of early-stage female breast cancer patients previously treated with WBRT. To maintain diversity of breast sizes and shapes, 13 right-sided and 17 left-sided cases with various breast volumes and separations were selected (Table 1). Every identifiable patient data was replaced with unique numbers as part of de-identification step, according to the centre’s ethics protocol.

Planning CT datasets were acquired using Philips CT Big Bore (Philips Healthcare, Best, The Netherlands) with patients lying supine on a lift-up board and arms raised above the head. Each slice of acquired CT datasets was 3 mm in thickness. Image registration and delineation of gross tumour volume (GTV), PTV and OARs were performed using Eclipse Treatment Planning System (TPS) (version 13.6.23; Varian Medical Systems, Palo Alto, CA, USA). GTV and PTV were contoured by the radiation oncologist. Contoured OARs included contralateral breast (CB), heart, liver, left lung, right lung, and total bilateral lungs. Lung volumes were contoured using auto-threshold function of the planning system. Heart volume was contoured based the heart atlas guidelines. Both CB and liver were delineated based on the visible breast and liver tissues, respectively.

2. Treatment planning

As conventional 3DCRT and incorporation of field-in-fields (3DFIF) is still considered to be the standard of care in breast cancer radiation treatment in many institutions, they were also included in this study for dosimetric comparison. For each dataset, 7 distinct plans, namely conventional 3DCRT, 3DFIF, Ecomp, Hybrid, tIMRT, IMRT MFS, and tVMAT were generated and compared against each other. In the case of Hybrid, tIMRT, IMRT MFS, and tVMAT treatment planning techniques, a separate structure encompassing the entire affected breast was contoured and labelled as IMRT PTV for each dataset. All treatment plans were produced in Eclipse TPS at RMIT University. A reference point at isocentre location was used to non-

| Table 1. Range of breast volumes and breast separations (n = 30) |
|-----------------|-----------------|
|                  | Mean ± SD       | Median (range) |
| Breast volume (cm$^3$) | 1,127.28 ± 559.54 | 1,089.78 (433.21–2,573.83) |
| Breast separation (cm) | 21.70 ± 2.72 | 21.76 (17.08–27.36) |

SD, standard deviation.
To normalize the dose. A prescription dose of 42.5 Gy in 16 fractions was applied for all planning techniques. Each treatment plan was created to meet the planning goals defined in Table 2.

1) 3DCRT and 3DFIF planning
3DCRT plans involved a pair of tangential fields with parallel opposing posterior fields and the choices of gantry angles for 3DCRT plans were selected to provide best PTV dose coverage while minimizing as much exposure as possible to adjacent OARs. Dynamic wedge angles and weightings used were selected to give the best PTV dose coverage and homogeneity. For all 3DCRT plans, 6-MV beams were used. Corresponding 3DFIF plan was created using the same gantry and collimator angles as 3DCRT plan for each patient CT dataset. One to two subfields were incorporated and shaped using multi-leaf collimators (MLCs) to remove any hot spots. For breast separation > 23 cm, 18-MV beams were included as subfield(s) to produce increased PTV dose coverage.

2) Ecomp planning
Ecomp plans were generated with the same tangential fields’ arrangement used in both 3DCRT and 3DFIF plans for each patient CT dataset. Addition of fluence was performed by incorporating irregular surface compensator for each tangential field. Selection of tissue penetration depth (TPD) for each irregular surface compensator was dependent on each patient’s breast separation. Skin flash was added for both fields to provide additional fluence beyond the skin surface. If required, manual fluence editing was also performed on case by case.

3) Hybrid planning
Hybrid plan consisted of a pair of open tangents supplemented with a pair of IMRT tangents with the same field parameters. Plan was normalized to 100% at reference point and manual fluence editing done as necessary.

4) tIMRT and IMRT MF5 planning
Gantry angles and field parameters for tIMRT plans were similar to Ecomp and the objective functions were specified accordingly to achieve the planning goals. For IMRT MF5 plans, 3 additional fields were incorporated in addition to the medial and lateral tangential fields, resulting in a total of 5 fields. Gantry angles were individually selected for each patient CT dataset to achieve optimal target coverage and minimize entry and exit dose to ipsilateral lung (IL), contralateral lung (CL), CB, and heart. Similar to tIMRT plan, IMRT MF5 plan was also optimized with objective functions specified to achieve the best attainable plan. Post-optimization improvements such as removal of hot spots, increasing PTV coverage and minimizing OARs dose were performed through manual fluence editing.

5) tVMAT planning
tVMAT plan utilized tangential with 50° dual arcs (Fig. 1). The gantry angles were chosen to achieve optimal PTV coverage and minimum OAR doses. Objective functions were specified accordingly to achieve plan objectives and dose constraints as illustrated in Table 2.

3. Plan comparison and statistical analysis
The parameters used for comparison of all plans were as shown in Table 3. Conformity Index (CI) and Homogeneity Index (HI) were

Table 2. Planning goals for PTV, IL, CL, CB, heart, and liver

| Structure | Planning goals |
|-----------|----------------|
| PTV       | Minimum dose (PTV_{Dmin}) = 95% dose (40.38 Gy) |
|           | Maximum dose (PTV_{Dmax}) = 107% dose (45.48 Gy) |
| IL        | Percentage volume of IL receiving 5 Gy (IL_{V5Gy}) < 60% |
|           | Percentage volume of IL receiving 20 Gy (IL_{V20Gy}) < 30% |
|           | Percentage volume of IL receiving 30 Gy (IL_{V30Gy}) < 10% |
| CL        | Percentage volume of CL receiving 10 Gy (CL_{V10Gy}) = 0% |
| CB        | Mean CB dose (CB_{Dmean}) < 2.5 Gy |
|           | Percentage volume of CB receiving 5 Gy (CB_{V5Gy}) < 15% |
| Heart     | Mean heart dose (Heart_{Dmean}) < 4 Gy |
|           | Percentage volume of heart receiving 5 Gy (Heart_{V5Gy}) < 40% |
|           | Percentage volume of heart receiving 20 Gy (Heart_{V20Gy}) < 10% |
| Liver     | Mean liver dose (Liver_{Dmean}) < 20 Gy |

PTV, planning target volume; IL, ipsilateral lung; CL, contralateral lung; CB, contralateral breast.

Fig. 1. Tangential 50° arcs in tangential volumetric modulated arc therapy plan. Each arc travels in opposing direction to each other (clockwise and anti-clockwise) to deliver dose to the entire breast volume.

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Table 3. Plan evaluation parameters for PTV, IL, CL, CB, heart, liver, MUs and the body

| Plan evaluation parameters | PTV | IL | CL | CB | Heart | Liver | MUs | Body |
|----------------------------|-----|----|----|----|-------|-------|-----|------|
| Conformity Index (CI)      |     |    |    |    |       |       |     |      |
| Homogeneity Index (HI)     |     |    |    |    |       |       |     |      |
| Maximum PTV dose (PTVmax)  |     |    |    |    |       |       |     |      |
| Percentage volume of PTV receiving 95% dose (PTV95%) | | | | | | | | |
| Mean IL dose (ILmean)      |     |    |    |    |       |       |     |      |
| Percentage volume of IL receiving 5 Gy (IL5Gy) | | | | | | | | |
| Percentage volume of IL receiving 20 Gy (IL20Gy) | | | | | | | | |
| Percentage volume of IL receiving 30 Gy (IL30Gy) | | | | | | | | |
| Mean CL dose (CLmean)      |     |    |    |    |       |       |     |      |
| Percentage volume of CL receiving 10 Gy (CL10Gy) | | | | | | | | |
| Mean CB dose (CBmean)      |     |    |    |    |       |       |     |      |
| Percentage volume of CB receiving 5 Gy (CB5Gy) | | | | | | | | |
| Percentage volume of IL receiving 5 Gy (IL5Gy) | | | | | | | | |
| Percentage volume of Il receiving 10 Gy (IL10Gy) | | | | | | | | |
| Mean heart dose (Heartmean) |     |    |    |    |       |       |     |      |
| Percentage volume of heart receiving 5 Gy (Heart5Gy) | | | | | | | | |
| Percentage volume of heart receiving 20 Gy (Heart20Gy) | | | | | | | | |
| Mean liver dose (Livermean) |     |    |    |    |       |       |     |      |
| Percentage volume of liver receiving 10 Gy (Liver10Gy) | | | | | | | | |
| Percentage volume of PTV receiving 95% dose (PTV95%) | | | | | | | | |
| Maximum PTV dose (PTVmax)  |     |    |    |    |       |       |     |      |

PTV, planning target volume; IL, ipsilateral lung; CL, contralateral lung; CB, contralateral breast; MUs, monitor units.

Calculated using the following formulas:

\[
CI = \frac{V_p}{TV}
\]

\[
HI = \frac{D_e}{D_{95}}
\]

\(V_p\) represents PTV volume in cm\(^3\) receiving 41.38 Gy or 95% of prescribed dose and TV represents PTV volume in cm\(^3\). \(D_e\) is minimum dose delivered to 5% of PTV and \(D_{95}\) is the minimum dose of 95% of PTV.

IBM SPSS Statistics version 25 (IBM Corporation, Armonk, NY, USA) was used for the statistical analysis to compare dosimetric parameters. One-way analysis of variance (ANOVA) tests were done to evaluate the dosimetric differences between all 7 techniques and post-hoc analysis was performed using Tukey’s honestly significant difference (HSD) test. Interactions between the planning techniques and breast volumes (<1,000 cm\(^3\) and >1,000 cm\(^3\)) were also evaluated using two-way ANOVA and Tukey’s HSD test for post-hoc analysis. Differences were considered as statistically significant when p-value is <0.05.

### Results

A total of 30 patients were included in this study, all diagnosed with early-stage malignant neoplasm of the breast prior to treatment. Age range of patients was between 34 and 78 years old. Outcomes for the PTV and OARs dosimetric parameters are shown in Table 4.

1. PTV dosimetry

There was a significant difference (p < 0.001) in PTVmax, amongst all techniques. PTVmax was significantly higher in 3DCRT, IMRT MF5, and tVMAT (p < 0.001), and above the limit of 107%. The difference among all 7 techniques in terms of PTV95% was statistically significant (p < 0.05). Significantly lower PTV95% was observed in tVMAT (p < 0.05) compared to other 6 techniques. CI was found to be significantly different (p < 0.05) among all techniques. tVMAT resulted in the significantly lower CI (p < 0.05) compared to all other techniques.

A significant difference (p < 0.001) was observed in terms of HI amongst all 7 techniques. Statistically significantly higher HI, hence poorer PTV dose homogeneity in 3DCRT, IMRT MF5, and tVMAT (p < 0.001) were observed when compared to the other techniques. Ecomp was also found to have the best PTV dose homogeneity as demonstrated by the HI value being closest to 1.0.

Breast volumes of each patient CT dataset was categorised into two groups: <1,000 cm\(^3\) and >1,000 cm\(^3\) to identify dosimetric differences on PTV dose conformity based on CI and dose homogeneity based on HI, as a result of interactions between the various techniques and breast volumes. It was shown that there was no statistically significant interaction between the effects of techniques and breast volumes. It was shown that there was no statistically significant interaction between the effects of techniques and breast volumes. It was shown that there was no statistically significant interaction between the effects of techniques and breast volumes. It was shown that there was no statistically significant interaction between the effects of techniques and breast volumes.

2. Ipsilateral lung dosimetry

Difference in IL\(_{\text{mean}}\) between the 7 techniques was found to be significant (p < 0.001). tVMAT had significantly highest IL\(_{\text{mean}}\) followed by IMRT MF5 (p < 0.001 for both) compared to other techniques. No significant difference was observed among techniques with tangential beams.

For IL\(_{\text{V5Gy}}\) it was also found to have significant difference among all techniques (p < 0.001). IL\(_{\text{V5Gy}}\) showed significantly highest for IMRT MF5 followed by tVMAT (p < 0.001 for both). Between IMRT MF5 and tVMAT, IMRT MF5 resulted in significantly higher IL\(_{\text{V5Gy}}\) (p < 0.001).

Difference in IL\(_{\text{V20Gy}}\) among all techniques was statistically signif-
Table 4. Dosimetric parameter outcomes for PTV and OARs, along with required planning times required between the various techniques

| Parameter | 3DCRT | 3DFIF | IMRT MF5 | tIMRT | tVMAT | Ecomp | Hybrid |
|-----------|-------|-------|----------|-------|-------|-------|--------|
| PTV_{39Gy} (Gy) | 46.01 ± 1.52 | 45.07 ± 0.36 | 46.38 ± 0.53 | 45.03 ± 0.69 | 46.35 ± 0.70 | 44.61 ± 0.71 | 44.87 ± 0.59 |
| PTV_{59Gy} (% | 98.19 ± 2.80 | 97.97 ± 3.02 | 99.05 ± 1.32 | 98.79 ± 2.01 | 95.73 ± 4.24 | 98.24 ± 2.69 | 98.59 ± 2.38 |
| Conformity Index | 0.98 ± 0.03 | 0.98 ± 0.03 | 0.99 ± 0.01 | 0.99 ± 0.02 | 0.96 ± 0.04 | 0.98 ± 0.03 | 0.98 ± 0.03 |
| Homogeneity Index | 0.98 ± 0.03 | 0.98 ± 0.03 | 0.99 ± 0.01 | 0.99 ± 0.02 | 0.96 ± 0.04 | 0.98 ± 0.03 | 0.98 ± 0.03 |
| H_{20Gy} (Gy) | 4.81 ± 2.48 | 4.70 ± 2.37 | 8.21 ± 1.01 | 4.86 ± 1.96 | 8.97 ± 2.24 | 5.18 ± 2.56 | 5.36 ± 2.38 |
| H_{5Gy} (% | 15.44 ± 7.84 | 15.61 ± 7.88 | 57.62 ± 9.20 | 16.84 ± 7.34 | 43.51 ± 9.87 | 17.50 ± 8.74 | 18.07 ± 8.35 |
| H_{2Gy} (% | 8.61 ± 5.69 | 8.58 ± 5.64 | 9.13 ± 3.79 | 9.23 ± 5.24 | 16.68 ± 5.64 | 9.94 ± 6.57 | 10.44 ± 6.51 |
| V_{5Gy} | 7.18 ± 5.24 | 7.06 ± 5.13 | 2.77 ± 2.09 | 6.44 ± 3.88 | 9.65 ± 4.50 | 7.37 ± 5.83 | 7.92 ± 5.05 |
| V_{30Gy} | 0.04 ± 0.03 | 0.04 ± 0.03 | 4.00 ± 1.56 | 0.04 ± 0.03 | 0.47 ± 0.32 | 0.05 ± 0.03 | 0.06 ± 0.03 |
| C_{12Gy} | 0.0 ± 0 | 0.0 ± 0 | 10.38 ± 6.84 | 0.0 ± 0 | 0.23 ± 0.55 | 0.0 ± 0 | 0.0 ± 0 |
| C_{2Gy} (Gy) | 8.02 ± 12.74 | 7.87 ± 12.03 | 22.00 ± 11.46 | 7.25 ± 11.47 | 27.61 ± 7.39 | 8.20 ± 12.64 | 9.29 ± 13.34 |
| C_{CB} (Gy) | 0.16 ± 0.12 | 0.17 ± 0.12 | 2.49 ± 1.83 | 0.14 ± 0.13 | 2.30 ± 2.08 | 0.18 ± 0.15 | 0.30 ± 0.53 |
| C_{CB} (Gy) | 0.12 ± 0.39 | 0.16 ± 0.53 | 14.52 ± 17.11 | 0.13 ± 0.43 | 14.86 ± 15.68 | 0.17 ± 0.50 | 0.18 ± 0.51 |
| Heart_{SPGy} | 1.52 ± 1.14 | 1.51 ± 1.11 | 4.20 ± 0.66 | 1.80 ± 0.74 | 4.98 ± 1.63 | 1.91 ± 0.96 | 2.15 ± 1.03 |
| Heart_{SPGy} | 2.97 ± 3.48 | 2.79 ± 3.11 | 23.90 ± 6.62 | 4.28 ± 3.03 | 25.28 ± 8.24 | 4.63 ± 3.76 | 5.00 ± 3.96 |
| Heart_{SPGy} | 1.45 ± 2.26 | 1.45 ± 2.26 | 1.12 ± 2.07 | 1.99 ± 1.95 | 6.80 ± 4.19 | 2.58 ± 2.52 | 2.89 ± 2.77 |
| Liver_{SPGy} (Gy) | 1.22 ± 1.78 | 1.20 ± 1.72 | 6.56 ± 4.02 | 1.48 ± 1.30 | 4.23 ± 3.05 | 1.69 ± 1.61 | 1.82 ± 1.48 |
| Liver_{SPGy} | 1.73 ± 4.19 | 1.76 ± 4.21 | 27.00 ± 20.02 | 3.00 ± 3.54 | 12.89 ± 10.27 | 3.27 ± 3.91 | 3.55 ± 3.94 |
| Body_{SPGy} | 8.07 ± 2.08 | 8.12 ± 2.10 | 16.71 ± 3.65 | 8.84 ± 1.82 | 13.40 ± 2.71 | 9.13 ± 1.97 | 9.29 ± 1.97 |
| Total MUs | 311 ± 21 | 303 ± 15 | 142 ± 19 | 500 ± 78 | 364 ± 49 | 520 ± 42 | 465 ± 53 |
| Planning time (min) | 14 ± 2 | 16 ± 2 | 80 ± 14 | 16 ± 2 | 39 ± 2 | 15 ± 3 | 18 ± 2 |

Values are presented as mean ± standard deviation.

PTV, planning target volume; OAR, organs-at-risk; 3DCRT, three-dimensional conformal radiation therapy; 3DFIF, three-dimensional field-in-field; IMRT MF5, 5-field intensity-modulated radiotherapy; tIMRT, tangential IMRT; tVMAT, tangential volumetric modulated arc therapy; Ecomp, electronic tissue compensation; IL, ipsilateral lung; CL, contralateral lung; CB, contralateral breast; MUs, monitor units.

Table 5. Comparison of PTV Conformity Index (Cl) and Homogeneity Index (HI)

| Technique | CI (p = 0.859) | HI (p = 0.550) |
|-----------|---------------|---------------|
|           | Breast volume < 1,000 cm³ | Breast volume > 1,000 cm³ | Breast volume < 1,000 cm³ | Breast volume > 1,000 cm³ |
| 3DCRT | 0.97 ± 0.04 | 0.99 ± 0.02 | 1.09 ± 0.03 | 1.09 ± 0.04 |
| 3DFIF | 0.98 ± 0.03 | 0.98 ± 0.03 | 1.07 ± 0.02 | 1.08 ± 0.04 |
| IMRT MF5 | 0.99 ± 0.01 | 0.99 ± 0.01 | 1.10 ± 0.01 | 1.09 ± 0.01 |
| tIMRT | 0.99 ± 0.02 | 0.99 ± 0.02 | 1.06 ± 0.03 | 1.07 ± 0.03 |
| tVMAT | 0.95 ± 0.04 | 0.96 ± 0.05 | 1.12 ± 0.03 | 1.11 ± 0.03 |
| Ecomp | 0.98 ± 0.03 | 0.99 ± 0.03 | 1.06 ± 0.03 | 1.06 ± 0.03 |
| Hybrid | 0.98 ± 0.02 | 0.99 ± 0.03 | 1.07 ± 0.03 | 1.08 ± 0.03 |

Values are presented as mean ± standard deviation.

PTV, planning target volume; 3DCRT, three-dimensional conformal radiation therapy; 3DFIF, three-dimensional field-in-field; IMRT MF5, 5-field intensity-modulated radiotherapy; tIMRT, tangential IMRT; tVMAT, tangential volumetric modulated arc therapy; Ecomp, electronic tissue compensation.

Statistically significantly higher IL_{V30Gy} was found in tVMAT (p < 0.001) in comparison to other techniques. The difference among all techniques was statistically significant for IL_{V30Gy} (p < 0.001). IMRT MF5 showed significantly reduced IL_{V30Gy} (p < 0.05) in comparison to other techniques.

3. Contralateral lung dosimetry

The difference among all techniques in terms of CL_{Vmean} was statistically significant (p < 0.001). IMRT MF5 was found to result in statistically significantly higher CL_{mean} (p < 0.001) compared to other techniques, close to 100 times higher than techniques with tangential fields arrangement. tVMAT followed as the second highest in terms of CL_{mean} and was approximately 10 times higher than 3DCRT, 3DFIF, tIMRT, Ecomp, and Hybrid. Among techniques using tangential fields arrangement, no significant difference was observed.
Fig. 2. Mean Conformity Index (CI) of all 7 techniques according to breast volumes. Error bars represent ±1 standard deviation. Black line over bars represents CI of 1.0 that represents ideal dose conformity to planning target volume. 3DCRT, three-dimensional conformal radiation therapy; 3DFIF, three-dimensional field-in-field; IMRT MF5, 5-field intensity-modulated radiotherapy; tIMRT, tangential IMRT; tVMAT, tangential volumetric modulated arc therapy; Ecomp, electronic tissue compensation.

Fig. 3. Mean Homogeneity Index (HI) of all 7 techniques according to breast volumes. Error bars represent ±1 standard deviation. Black line over bars represents HI of 1.0 that represents ideal dose homogeneity in planning target volume. 3DCRT, three-dimensional conformal radiation therapy; 3DFIF, three-dimensional field-in-field; IMRT MF5, 5-field intensity-modulated radiotherapy; tIMRT, tangential IMRT; tVMAT, tangential volumetric modulated arc therapy; Ecomp, electronic tissue compensation.
Similar to $CL_{\text{Dmean}}$, difference in $CL_{V10Gy}$ was also statistically significant among all techniques ($p < 0.001$). IMRT MF5 produced significantly increased $CL_{V10Gy}$ ($p < 0.001$) compared to others.

4. Contralateral breast dosimetry

Difference among the 7 techniques was statistically significant ($p < 0.001$) for $CB_{\text{Dmean}}$. Both tVMAT and IMRT MF5 ($p < 0.001$ for both) resulted in statistically significantly increased $CB_{\text{Dmean}}$. However, both were not significantly different from each other. There was also no statistically significant difference in $CB_{\text{Dmax}}$ demonstrated between the techniques with tangential beams.

$CB_{\text{Dmean}}$ of all techniques were significantly different ($p < 0.001$). $CB_{\text{Dmean}}$ was significantly higher in IMRT MF5 and tVMAT ($p < 0.001$ for both) compared to other techniques, however both were not different from each other.

$CB_{V5Gy}$ of all techniques were also shown to be statistically significantly different ($p < 0.001$). tVMAT and IMRT MF5 ($p < 0.001$ for both) resulted in almost 100 times significantly higher $CB_{V5Gy}$ compared to other 5 techniques with tangential beams, however, were not significantly different from each other.

5. Heart dosimetry

The difference in $Heart_{\text{Dmean}}$ among all 7 techniques was statistically significant ($p < 0.001$). Statistically significantly increased $Heart_{\text{Dmean}}$ was observed in tVMAT and IMRT MF5 ($p < 0.001$ for both) and were beyond the dose tolerance goal limit of 4 Gy. However, no significant difference was observed between both techniques. Between techniques with tangential fields arrangement, no statistically significant difference was found.

In terms of $Heart_{V20Gy}$, the difference between all techniques was also significant ($p < 0.001$). Significantly higher $Heart_{V20Gy}$ in tVMAT and IMRT MF5 ($p < 0.001$ for both) were observed, approximately 5 to 10 times greater than other 5 techniques.

For $Heart_{V20Gy}$, the difference among all techniques was significant ($p < 0.001$). tVMAT demonstrated significantly highest $Heart_{V20Gy}$ compared to other techniques ($p < 0.001$).

6. Liver dosimetry

IMRT MF5 resulted in significantly higher $Liver_{\text{Dmean}}$ ($p < 0.001$) compared to 3DCRT, 3DFIF, tIMRT, Ecomp, and Hybrid. tVMAT ($p < 0.05$) also had significantly higher $Liver_{\text{Dmean}}$ compared to 3DCRT and 3DFIF; however, was not significantly different from tIMRT, Ecomp, Hybrid, and IMRT MF5. The remaining 5 techniques adopting the tangential fields configuration showed similar $Liver_{\text{Dmean}}$ and were not significantly different from each other.

$Liver_{V10Gy}$ was also significantly different between the various techniques ($p < 0.001$). IMRT MF5 demonstrated statistically significantly highest $Liver_{V10Gy}$ among all techniques ($p < 0.005$). tVMAT ($p < 0.05$) also had significantly higher $Liver_{V10Gy}$ compared to 3DCRT and 3DFIF, however was not statistically significantly different from other intensity-modulated techniques—tIMRT, Ecomp, and Hybrid. Reduced $Liver_{V10Gy}$ was observed among techniques with tangential beams, however no significant difference was observed among them.

7. Total monitor units, body low dose and planning time comparisons

Difference in total monitor units (MUs) produced by all 7 techniques was statistically significant ($p < 0.001$). Statistically significantly highest total MUs was observed in IMRT MF5 ($p < 0.001$). 3DCRT, 3DFIF, and tVMAT were shown to produce significantly lower total MUs ($p < 0.001$ for all three) but were not significantly different from each other. Those utilizing intensity-modulated beams (tIMRT, Ecomp and Hybrid), resulted in significantly higher total MUs ($p < 0.001$ for all three). However, they were also not significantly different from each other.

Statistically significant increase in $Body_{V10Gy}$ of approximately twice the amount was observed in IMRT MF5 and tVMAT ($p < 0.001$ for both) among all techniques.

To evaluate the efficiency of each technique, planning times for the various techniques were also recorded and compared (Table 4). Planning times for all studied techniques were significantly different ($p < 0.001$). Among all techniques, IMRT MF5 required the longest planning time followed by tVMAT ($p < 0.001$ for both). IMRT MF5 was significantly longer ($p < 0.001$) to plan than tVMAT. 3DCRT and Ecomp were techniques with shortest planning times.

Discussion and Conclusion

To date, no study had been carried out that performed a direct comparison of conventional 3DCRT and 3DFIF with more advanced techniques: Ecomp, Hybrid technique, various numbers of IMRT beams and use of tangential arc arrangements in VMAT, as part of an entire study of radiation therapy to both left and right early-stage breast cancer cases. In this study, PTV and OARs dosimetry were used as parameters for direct comparison between 3DCRT, 3DFIF, IMRT MF5, tIMRT, tVMAT, Ecomp, and Hybrid techniques.

It is essential that $PTV_{\text{Dmax}}$ is kept to <107% (45.48 Gy) to achieve the desired dose uniformity eventually to reduce risk of skin reactions. Results obtained in this study demonstrated that only 3DFIF, tIMRT, Ecomp, and Hybrid were able to meet the constraint of $PTV_{\text{Dmax}} < 107\%$, with Ecomp having the lowest $PTV_{\text{Dmax}}$.

IMRT MF5 produced highest $PTV_{V95\%}$ compared to other tech-
niques, indicating improved dose coverage. This was consistent with the findings in some studies that increasing number of IMRT beams would increase PTV dose coverage [13–15]. As PTV CI was directly correlated to $PTV_{V95\%}$, it was hence not surprising that IMRT MF5 also similarly showed highest CI among all techniques. Despite having the highest $PTV_{V95\%}$ and CI value closest to the ideal value of 1.0, IMRT MF5 did not show any significant difference in comparison with techniques using tangential beams. This indicates that although increasing number of beams as seen in IMRT MF5 showed increased $PTV_{V95\%}$ and CI, it is however comparable to techniques using only tangential beams.

tVMAT showed the statistically significantly worst performance for $PTV_{V95\%}$ and CI. This was in contrary to the findings reported by Zhao et al. [16], Lin et al. [17], and Qiu et al. [18] that VMAT resulted in improved CI than IMRT and 3DCRT plans. This discrepancy can be attributed to the varied arc arrangement used in this study compared to those used by the above-mentioned studies. As a matter of fact, Viren et al. [19] found that use of a pair of 50° dual arcs, similar to that used in this study, resulted in lower target dose coverage and conformity compared to the use of continuous arc arrangement employed by most studies.

Previous reports stated Ecomp as providing improved target dose homogeneity, especially over the conventional 3DCRT [20–22]. This was observed as true in this study, with Ecomp producing the best HI among all techniques, having the value closest to the ideal value of 1.0. Zaghoul et al. [23] reported a correlation between improved PTV HI and significant reduction of acute skin reaction incidence. This correlation between the clinical outcome and PTV HI can be applicable to the findings in this study that indicates Ecomp as having the potential of reducing risk of acute skin toxicities compared to the other techniques. In contrast, tVMAT and IMRT MF5 were observed to give statistically significantly poorest PTV HI. Poorer PTV dose homogeneity observed in both tVMAT and IMRT MF5 could be due to number of beams and the configurations of arcs and beams used. The use of optimizer and OARs constraint-based process involved, could have also further contributed to the overall poorer PTV dose homogeneity. In the attempt of meeting the OARs dose constraint, optimization-convergence errors were likely to have occurred [24], especially due to the major tissue density difference present between the breast tissue and air in the lungs. Thus, in the optimizer’s attempt of achieving various constraints of OARs that also included the low-density lungs, heterogenous regions of high and low doses (hot and cold spots) were formed within the PTV.

Previous studies also reported a correlation in breast volume and dose homogeneity [25–27]. Large breast volumes tend to involve reduced dose homogeneity and increased high dose regions within the PTV that result in acute skin toxicity [15,26]. In this study, it was found that there was no statistically significant interaction between the effects of variations in breast volumes and techniques on both CI and HI. However, there were significant differences on PTV CI and HI between various techniques. This indicates that only variations in techniques affect CI and HI, and that they do not vary according to breast volumes.

In this study, IMRT MF5 had the highest $IL_{V20Gy}$ and lowest $IL_{V30Gy}$ among all techniques. These findings corroborate with the data reported by Liu et al. [28] that showed 5-field IMRT was able to reduce the $IL_{V20Gy}$ and $IL_{V30Gy}$ in comparison to 3DCRT with tangential beams. In terms of CL exposure, IMRT MF5 also showed significantly highest $CL_{O	ext{mean}}$ and $CL_{V95\%}$. Such findings are similar to that presented by Rongsriyam et al. [29] in which $CL_{O	ext{mean}}$ was also found to be much higher in IMRT than in 3DCRT. These results were expected due to greater number of beams involved that resulted in increased beam entry and exit through CL, hence the dose contribution. This implies that success of IMRT MF5 in reducing the volumes of lungs receiving high doses comes at the expense of overall higher mean dose and greater volumes receiving the low dose.

Use of arcs in VMAT in previous studies [14,30] was similarly found to result in significantly higher low-dose volume, especially to IL, which is also observed in this present study. In general, this highlights that non-tangential beams techniques result in increased lungs exposure, thus greater implication in future development of pulmonary complications. Techniques with tangential beams are in contrast, comparably similar to each other in improving lung sparing, hence reducing the likelihood of radiation pneumonitis and secondary lung cancer post-radiotherapy.

Some studies have reported that IMRT reduced the CB dose compared to conventional 3DCRT [31,32]. This was found to be true in this study, with tIMRT showing lower CB doses than 3DCRT. However, it is not the case for IMRT MF5 due to greater number of fields used that resulted in low dose spill to greater CB volume. This can be of high importance, especially to patients <40 years old who are at greater risk of secondary CB cancer [33]. Similar to the results in this study, other papers have also reported that use of VMAT resulted in high low-dose volume to CB [14,34], hence also posing the issue of greater risk of inducing secondary CB cancers especially to younger patients. The application of techniques with tangential beams in contrast, introduces a greater advantage of improved CB dosimetry, thus reduced risk of inducing secondary CB cancers.

In this study, all studied techniques were able to meet the constraint of $Heart_{O	ext{mean}}$ of <4 Gy, except for IMRT MF5 and tVMAT. Both the above techniques were also found to result in higher $Heart_{V5Gy}$ compared to the rest. These findings are similar to those
by Liu et al. [28] who found that 5-field IMRT and double-arcs VMAT both had higher heart doses compared to 3DCRT. This present study showed reduced heart doses with techniques utilizing tangential beams, hence once again highlighting the advantage of improved organ sparing compared to the use of multi-fields or arcs utilizing techniques.

Radiation-induced liver disease (RILD) is often described as a significant complication and major limitation of liver cancer radiation treatment [35]. Although the whole liver is not directly irradiated in breast radiation therapy, liver toxicity is a factor that must still be taken into consideration in right-sided breast radiation therapy due to its close proximity to PTV. In this study, the number of right-sided patient cases is less than left-sided cases, however the results positively showed a significant reduction of liver doses in 3DCRT, 3DFIF, tIMRT, Ecomp, and Hybrid compared to IMRT MF5 and tVMAT. Higher liver doses observed in IMRT MF5 and tVMAT can be attributed to greater low dose volume caused by increased number of intensity-modulated fields, greater field scattering and dose leakage between the MLC leaves [28]. Techniques utilizing tangential beams are in contrast better for liver sparing and thus able to reduce the risk of RILD.

IMRT MF5 showed significantly highest total MUs, almost 5 times of the conventional 3DCRT and 3DFIF. Other techniques similarly using intensity-modulated fields (tIMRT, tVMAT, Ecomp, and Hybrid) also showed higher MUs than 3DCRT and 3DFIF. This was expected because intensity-modulated techniques involve large numbers of small subfields to achieve optimum intensity distributions of each treatment field [36], thus resulting in higher MUs compared to non-intensity modulated 3DCRT and 3DFIF. With increase in the number of intensity-modulated beams, it was not surprising that IMRT MF5 resulted in highest total MUs.

In this study, IMRT MF5 had the highest $\text{Body}_{V_{10Gy}}$, followed by tVMAT. Involvement of more beams and therefore larger volume of normal tissues exposed to the low dose as demonstrated with higher $\text{Body}_{V_{10Gy}}$ was thus expected of IMRT MF5. Although tIMRT, Ecomp, and Hybrid are also intensity-modulated techniques, the lower MUs involved provided the advantage of lower $\text{Body}_{V_{10Gy}}$ that are comparable to conventional 3DCRT, hence pose no increased risk of inducing secondary cancers compared to conventional 3DCRT and 3DFIF.

tVMAT has lower MUs than all other intensity-modulated techniques and is similar to that of 3DCRT and 3DFIF. However, it still resulted in second highest $\text{Body}_{V_{10Gy}}$. This finding is attributed to the arc motion that produces dose fall-off occurring in every direction, therefore distributing low doses to bigger volumes of normal tissues, resulting in subsequent increased risk of secondary cancer induction. This observation is similar to a study conducted by Abo-Madyan et al. [37] who found that in comparison with 3DCRT, VMAT resulted in higher cumulated excess absolute risk of developing secondary malignancies after exposure to low doses. Based on the analysis, use of tIMRT, Ecomp, and Hybrid as alternatives to 3DCRT and 3DFIF pose no increased risk of inducing secondary malignancies due to comparable smaller body volumes receiving low doses. IMRT MF5 and tVMAT however, can potentially increase the risk due to greater body volume exposed to low doses.

A large number of early-stage breast cancer patients is often observed in a typical radiation therapy department. This implies that techniques with increasing complexity will affect the department’s resource allocation. To determine the department’s resource efficiency, parameters such as treatment and planning times were often used [38]. Under clinical setting, total MUs are associated with treatment time. Though this study is a planning study that does not constitute treatment delivery, the results suggest that IMRT MF5 is the technique that would require longest treatment time while techniques with lowest MUs (3DCRT, 3DFIF and tVMAT) would result in shortest treatment time.

In terms of planning time, this study similarly revealed that IMRT MF5 requires the longest time followed by tVMAT. This was due to the process of adjusting the field and arc arrangements, along with iterative optimization processes to achieve the best plans. Planning times for tIMRT and Ecomp are in contrast, comparable to conventional 3DCRT and 3DFIF. However, as tIMRT requires inverse-planning, similar to IMRT MF5, tVMAT and Hybrid, additional steps of contouring of the IMRT structures are required for the optimization process. The planning times recorded for these inverse-planned techniques in this study do not include the duration required to contour those IMRT structures. Since Ecomp is a forward-planned technique, that additional time of contouring the IMRT structures is not required, hence is more superior than the other advanced techniques in terms of time-efficiency. When looking at studies published on Ecomp, it was also suggested that electronic compensation algorithm used for Ecomp is a feature found only in Eclipse TPS. Hence, institutions using other TPS might not be able to implement the use of Ecomp as an alternative WBRT technique.

Based on the analyses, techniques with tangential beams result in significant reduction of OARs doses compared to those using multiple beams and arcs as demonstrated in IMRT MF5 and tVMAT. In terms of PTV dose coverage, conformity and homogeneity, tIMRT, Ecomp, and Hybrid are more superior than 3DCRT and 3DFIF and are also comparable to conventional 3DCRT and 3DFIF in the OARs doses. However, it is noted that Hybrid led to higher contribution of low-doses to IL, CL, CB, heart, and liver compared to tIMRT and Ecomp, indicating a possible clinical significance of increased risk of long-term complications and secondary cancer induction. This
was similarly observed in the studies conducted by Mayo et al. [39] and Xie et al. [40] who found that improvements of PTV dosimetry in Hybrid were achieved at the expense of increased low-dose volume to the CB, lungs and heart compared to tangential IMRT-only technique.

Out of the three, Ecomp required comparably shorter planning time. Use of skin flash tool incorporated in Ecomp also further helps to account for patient’s breathing motion, increasing the accuracy of dose delivery. Overall, this highlights the potentially better patient outcome and subsequently improved patient’s QOL. Therefore, Ecomp shows promising use in terms of efficiency and effectiveness and may be favoured as an optimal technique for WBRT in departments where Eclipse planning system is available.

This study focusses exclusively on early-stage breast cancer patients treated with WBRT without any regional lymph nodes involvement. Hence, the current results might not be applicable for patients requiring treatments to both breast and the regional nodes. A greater number of patient cases and inclusion of patient groups requiring breast and nodal radiation therapy should therefore be done in future studies to better evaluate the results and draw more definitive conclusions.

In conclusion, techniques with tangential fields arrangement resulted in overall better OARs dosimetry compared to those with multi-fields and arcs arrangements. Of all the techniques used in this study, Ecomp emerged as a better treatment technique for WBRT in terms of both effectiveness and efficiency. However, this study is a retrospective planning study and therefore the planning dosimetric data obtained might be different from actual delivered doses to patients in real-life clinical situations. Further studies involving water phantom simulation and/or clinical applications on patients are hence required to better compare and verify the dosimetric results obtained in this study.

Conflict of Interest

No potential conflict of interest relevant to this article was reported.

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