INTRODUCTION

Dentin caries is classified into infected dentin and affected dentin [1,2]. Infected dentin is the outermost layer of caries consisting of a mineral matrix and hydroxyapatite crystals which are destroyed by a bacterial infection and its byproducts. The damage is irreversible and inhibits remineralization. By contrast, affected dentine is the inner layer that is partially demineralized, but the damage is still reversible. The affected dentine zone can undergo demineralization as it contains healthy collagen fibrils surrounded by hydroxyapatite crystals and collagen crosslinks [2,3]. Dentin remineralization can occur due to the deposition of minerals between collagen fibers [4].

Remineralization can occur through two methods: Conventional remineralization and guided-tissue remineralization (GTR). Conventional remineralization occurs through epitaxial growth of mineral crystals present in demineralized lesions [5], whereas GTR is a method of extrabovular and intrafibrillar collagen dentin mineralization in calcium phosphate phase [6]. Non-collagen proteins play a very important role in stabilizing the amorphous calcium phosphate (ACP) formation which does not form aggregates and stays in nano [4,7]. Dentin matrix protein 1 (DMP1), a non-collagen protein with a high affinity for calcium ions, is actively involved in regulating mineral formation by interacting with collagen fibrils through electrostatic bonds and plays a key role in mineral formation in the intrafibrillar and extrafibrillar spaces [8]. However, DMP1 can be damaged by caries, and an analogous material is needed to replace the damaged DMP1. Analogous materials for remineralization must contain multiple phosphate and carboxyl groups that can bind to calcium [7]. Several such analogous materials are known to be able to mimic the function of DMP1 non-collagen protein [4].

Recently, polymer-induced liquid-precursor (PILP) has been developed as a process involved in GTR [2,9,10]. This process is known as a rapid biomimetic remineralization process and uses synthetic anionic polymer materials that can replace the role of non-collagen proteins in intrafibrillar remineralization process [11,12]. These polymers play an important role in the phase of liquid mineral precursors. Fluids easily fill the gaps in collagen fibrils, with the remineralization of collagen fibrils, and the resulting nanodroplets [10–15] diameter diffusing into type 1 collagen intrafibrillar or gap zone [2,13]. Polyspartic acid, a non-collagen protein analog necessary for the PILP process, is a negatively charged amino acid synthesized using non-toxic and biodegradable materials [4,14].

Remineralization of intrafibrillar collagen can be visualized using transmission electron microscopy (TEM). A TEM is an electron microscope that works by passing electrons through the object of observation and obtains information in the form of images [7,15]. In addition, the average size and crystallinity of a sample can be examined using the X-ray diffraction (XRD) technique [5].

METHODS

The research protocol used in this study (Protocol No. 0512111218) was approved by the Ethics Committee of Faculty of Dentistry, Universitas Indonesia. After extraction, the teeth were immediately immersed in deionized water at a temperature of 40°C. The samples were divided into four groups. Group I (control) represented demineralized dentin (without remineralization), whereas Groups II, III, and IV (treatment groups) were subjected to remineralization for 3, 7, and 14 days, respectively.

In the control group, the dentin block was soaked in demineralization solution (40 ml of 0.05 M acetic buffer containing 2.2 mM calcium phosphate [pH 5]) for 66 h. In the treatment groups, 40 ml of remineralization solution containing 50 mM of Tris buffer, 0.9% NaCl, 0.02% NaN₃, 4.5 mM CaCl₂, and 2.1 mM K,HPO₄ was used. Then, 4 mg of polyspartic acid powder (molecular weight = 23 kDa, 100 µg/ml;
Alamanda Polymer USA) was mixed into the solution and incubated at 37°C by shaking it continuously for 3, 7, or 14 days. The samples were analyzed using XRD to determine the size of hydroxyapatite crystals and TEM to observe intrafibrillar remineralization, which can be detected based on the occurrence of mineral deposits in dentin collagen intrafibrillar.

The data were analyzed using the normality distribution test in each group using the Shapiro-Wilk test. Furthermore, the Kruskal–Wallis test was used to determine differences among the four groups. All statistical analyses were carried out using the SPSS 22 software, at a significance level of p<0.05.

RESULTS AND DISCUSSION

In this study, the remineralization of demineralized dentin using polyaspartic acid in the PILP process was evaluated using XRD and TEM. The TEM was performed to visualize the occurrence of intrafibrillar remineralization characterized by mineral deposits in the intracellular collagen. The XRD examination was carried out to evaluate the size of hydroxyapatite crystals [16].

In all groups, the size of hydroxyapatite crystals was smaller than 40 nm (Table 1), i.e., smaller than the size of the gap zone filled with hydroxyapatite crystals in collagen fibrils, as shown previously [1,7]. However, the number of hydroxyapatite crystals is more important than the size. Crystals nucleate and grow to a certain extent depending on the Gibbs free energy [5]. The relatively small size of crystals (<40 nm) in all samples indicates that remineralization has entered the intrafibrillar area to produce nanometer crystals. Next, we performed TEM to visualize the occurrence of intrafibrillar remineralization.

Fig. 1 shows an elongated amorphous demineralized dentine, which indicates the presence of collagen (blue arrow) and a few crystals, which appeared as black dots (black arrows). Demineralization that occurs is partially demineralized. In general, crystals in intrafibrillar collagen still remain [1].

Table 1: Average size of hydroxyapatite crystals in various groups

| Sample  | Demineralized dentin control group | Remineralization groups |
|---------|-----------------------------------|-------------------------|
| Sample 1 | 30.455                            | 30.987 25.375 38.381 |
| Sample 2 | 19.449                            | 29.933 8.180 25.379 |
| Sample 3 | 30.455                            | 25.997 25.384 30.458 |
| Sample 4 | 27.109                            | 32.659 25.376 30.457 |

Fig. 2 shows regular elongated collagen (blue arrow) and the presence of more black dots (black arrows) indicating the entry of mineral deposits in the intrafibrillar space. This proves that intrafibrillar remineralization has begun.

Collagen observed after 7 days of remineralization was elongated and striated (Fig. 3, blue arrow) resembling collagen in healthy dentine. In addition, several black dots were observed in the collagen indicating an increase in the number of mineral deposits that entered the gap zone (black arrows). Increasingly dark collagen was observed after 14 days of remineralization (Fig. 4, blue arrow) indicating that mineral deposits that entered the gap zone filled the collagen intrafibrillar space (black arrows). Changes in TEM images (Figs. 1-4) indicate remineralization of intrafibrillar collagen.

In this study, we aimed to determine the occurrence of dentine remineralization after the application of polyaspartic acid, which was able to remineralize the affected dentine during the PILP process and resulted in intrafibrillar and extrafibrillar remineralization [1,3,17].

Remineralization of dentine using the GTR method involves reconstruction of two components: Type I collagen and apatite minerals. Collagen functions as a scaffold for the deposition of apatite [4,7]. In addition, non-collagen proteins play an important role in binding to collagen and stabilizing ACP by preventing the release of calcium and phosphate.
In this study, polyaspartic acid was used as a non-collagen protein analog, as it is biocompatible, biodegradable, and non-toxic. Because of the presence of a carboxyl group, polyaspartic acid showed a high affinity for calcium ions [4,6]. Polyaspartic acid also plays a role in stabilizing the ACP by preventing its aggregation and maintaining its nanosize. Then, the nanocomplex entered intrafibrillar collagen and forms hydroxyapatite crystals resulting in intrafibrillar remineralization [5]. According to the previous studies, excess intrafibrillar remineralization improves the mechanical properties of dentine [1,2]. Intrafibrillar minerals are more resistant to demineralization, and dentin collagen with high intrafibrillar mineral concentration has a high modulus of elasticity [4].

The size of hydroxyapatite crystals in each sample was smaller than 40 nm, as examined by XRD (Table 1) [18]. Fibrils contain a 40-nm gap zone, which is filled with intrafibrillar minerals [18]. The size of hydroxyapatite crystals below 40 nm implies that the crystals can enter the gap zone or collagen intrafibrillar space [1]. No significant differences were detected in the size of hydroxyapatite crystals among the four groups; this is consistent with the theory of Gibbs free energy, which states that crystals have a limited ability to grow [15]. The size below 40 nm also proves that polyaspartic acid, the non-collagen protein analog used in this study, can maintain ACP formation and prevents the aggregation of ACP nanoparticles into larger particles [6]. The polyaspartic acid-ACP nanocomplex is capable of penetrating the gap zone and forming hydroxyapatite crystals.

To ensure the occurrence of intrafibrillar remineralization, we performed TEM [7]. The use of polyaspartic acid as a substitute for DMP1 to induce intrafibrillar remineralization is evident by TEM (Figs. 1-4). Fig. 1 shows irregular collagen, indicating that collagen is degraded by the loss of most minerals. The demineralization is partial; therefore, some crystals remain in the intrafibrillar collagen. Collagen acts as a scaffold for the nucleation and growth of hydroxyapatite crystals [7]. Fig. 2 shows the entry of calcium and phosphate mineral deposits in the intrafibrillar space after 3 days of remineralization indicating the start of intrafibrillar remineralization. Mineral precursors could enter into the gap zone and diffuse along fibrils within 24 h. Furthermore, apatite crystals are formed along collagen fibrils on horse tendons within 72 h [13]. The collagen in Fig. 3 resembled that in healthy dentine with elongated and striated features after 7 days of remineralization. In addition, many black dots appeared in the collagen, indicating an increase in the number of mineral deposits in the gap zone. This indicates that the remineralization of intrafibrillar collagen increases with time. Fig. 4 shows the presence of darker collagen after 14 days of remineralization indicating that the mineral deposits that enter the gap zone gradually fill the intrafibrillar collagen space.

The formation of ACP precursors is an important stage in biomineralization [2]. Fibril collagen acts as a scaffold for intrafibrillar mineralization [1,4,19]. Gower et al. (2012) showed that ACP diffuses into the collagen in the liquid form via capillary action [13]. However, infiltration of ACP into collagen is mediated by the interaction of the charge between the complex minerals and certain areas of collagen fibrils [4,13]. Interaction occurs between the negatively charged polymer–mineral complex and positively charged gap zone [5]. ACP precursors stabilized by the negatively charged polymers in the form of nanodroplets interact with positive charges along with collagen molecules and stimulate compaction and nucleation of ACP in collagen. The nucleation of ACP develops and matures into apatite nanocrystals along with the collagen intrafibrillar space [4,19]. This was clearly observed by TEM, especially in Fig. 4.

**PILP** is known as a fast remineralization process and uses synthetic anionic polymers that can replace the role of non-collagen proteins in the intrafibrillar remineralization process [2,20]. Polyaspartic acid plays an important role in remineralization because it is able to bind to positively charged calcium ions through its negatively charged carboxyl group [4,6]. Our PILP study provides a strong foundation for developing dental materials that play a key role in the remineralization of dentine intrafibrillar collagen; for example, a superior restoration material for the remineralization of intrafibrillar dentine collagen in the cavities affected by dentine. Further research is needed to investigate the strength of collagen formed by remineralization.

**CONCLUSION**

The size of hydroxyapatite crystals formed after 3, 7, and 14 days of remineralization was similar in size (average 20–30 nm). Intrafibrillar remineralization started on the 3rd day and increased with time, as indicated by the presence of mineral deposits on intrafibrillar collagen after remineralization with polyaspartic acid in the PILP process.

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