Vascular permeability, vascular hyperpermeability and angiogenesis

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Abstract The vascular system has the critical function of supplying tissues with nutrients and clearing waste products. To accomplish these goals, the vasculature must be sufficiently permeable to allow the free, bidirectional passage of small molecules and gases and, to a lesser extent, of plasma proteins. Physiologists and many vascular biologists differ as to the definition of vascular permeability and the proper methodology for its measurement. We review these conflicting views, finding that both provide useful but complementary information. Vascular permeability by any measure is dramatically increased in acute and chronic inflammation, cancer, and wound healing. This hyperpermeability is mediated by acute or chronic exposure to vascular permeabilizing agents, particularly vascular permeability factor/vascular endothelial growth factor (VPF/VEGF, VEGF-A). We demonstrate that three distinctly different types of vascular permeability can be distinguished, based on the different types of microvessels involved, the composition of the extravasate, and the anatomic pathways by which molecules of different size cross-vascular endothelium. These are the basal vascular permeability (BVP) of normal tissues, the acute vascular hyperpermeability (AVH) that occurs in response to a single, brief exposure to VEGF-A or other vascular permeabilizing agents, and the chronic vascular hyperpermeability (CVH) that characterizes pathological angiogenesis. Finally, we list the numerous (at least 25) gene products that different authors have found to affect vascular permeability in variously engineered mice and classify them with respect to their participation, as far as possible, in BVP, AVH and CVH. Further work will be required to elucidate the signaling pathways by which each of these molecules, and others likely to be discovered, mediate the different types of vascular permeability.

Keywords Vascular permeability · Basal vascular permeability · Acute vascular hyperpermeability · Chronic vascular hyperpermeability · VEGF-A · VVO · Angiogenesis

Introduction

All cells require a continuing supply of nutrients and a means of clearing waste products. Single cells achieve these necessities by exchanging gases and small molecules directly with their environment by diffusion. However, vertebrates have solved the problems of nutrition and waste disposal by developing a vascular system that extends into all organs and tissues. While the vascular system of higher organisms is often described as “closed”, it needs to be sufficiently “open” (i.e., “permeable”) to allow the ready exchange of small molecules (gases, nutrients, waste products) with the tissues. Plasma proteins also need to
cross the normal vascular barrier, at least in small amounts. Albumin, for example, transports fatty acids and vitamins and immunoglobulin antibodies are required for host defense.

Vascular permeability, then, is essential for the health of normal tissues and is also an important characteristic of many disease states in which it is greatly increased. Examples are acute inflammation and pathologies associated with angiogenesis such as tumors, wounds, and chronic inflammatory diseases [1–4]. However, there is considerable disagreement as to the meaning of the term vascular permeability and the methods by which it should be measured [5]. Also, permeability is an extremely complicated process that, however defined, is affected by many different variables. These include the intrinsic properties of the different types of microvessels involved (capillaries, venules, mother vessels (MV)); the size, shape, and charge of extravasating molecules; the anatomic pathways molecules take in crossing the endothelial cell barrier; the time course over which permeability is measured; and the animals and vascular beds that are being investigated. This review addresses these issues with the hope that investigators in different fields will be able to communicate more effectively with each other and better measure and evaluate the significance of vascular permeability in normal physiology and in various pathologic states. A closely related issue, that of the passage of inflammatory cells across the microvasculature, is discussed elsewhere [6–8].

What is vascular permeability and how should it be measured?

The physiologists’ view of vascular permeability

Surprisingly, there is not good agreement as to what is meant by the term “vascular permeability” and from this it follows that there is no consensus about how vascular permeability should be measured. Over the last half-century eminent physiologists including Pappenheimer, Landis, Starling, Renkin, Michel, Curry, Rippe, and Bates have investigated the mechanisms by which plasma and its solutes cross the vascular barrier [5, 9–13]. They recognized that capillaries were the vascular segment involved in molecular exchange in normal tissues and that gases, water, and other small molecules crossed the capillary endothelial cell barrier freely whereas the passage of larger molecules such as plasma proteins was tightly restricted. Physiologists have commonly regarded capillary endothelium as a passive barrier, a thin, cellophane-like membrane that is punctuated by large numbers of small pores and lesser numbers of large pores. They postulated that the numerous small pores allowed the ready passage of small molecules and that the lesser number of large pores allowed limited extravasation of plasma proteins. With these assumptions in mind they developed elegant methods for investigating the flux of water and of plasma solutes across individual cannulated microvessels. They developed equations to calculate the three parameters that determine permeability, namely, hydraulic conductivity, reflection coefficient, and diffusion. Diffusion is the most important of these for the exchange of small molecules and is driven by the molecular concentration gradient across vascular endothelium as determined by the Fick equation:

$$J_s = DA/[C_v - C_i]$$

where $J_s$ is the diffusion rate (e.g., ml/s) of a particular solute; $D$ is the diffusion coefficient for that solute; $A$ is surface area available for exchange; $T$ is the thickness of the capillary; and $C_v - C_i$ is the difference in solute concentration between the plasma and the interstitial fluid.

The value of $D$ in the Fick equation depends heavily on molecular size; for example, the diffusion of albumin across the vasculature is estimated to be ~1,000-fold less than that of water [11, 12]. As a result, filtration is much more important than diffusion for the flux of large molecules such as plasma proteins and is determined by the Starling equation:

$$J_v = LpA[(P_v - P_i) - \sigma(\pi_v - \pi_i)]$$

where $J_v$ is filtration rate (e.g., ml/s); $L_p$ is hydraulic conductivity or the filtration coefficient, a property of the capillary wall and a measure of capillary permeability to water; $A$ is surface area available for molecular exchange; $P_v - P_i$ and $\pi_v - \pi_i$ are, respectively, the hydrostatic and osmotic pressure differences between the plasma and the interstitium; and $\sigma$ is the osmotic reflection or solvent-drag reflection coefficient. $\sigma$ varies in different tissues from 0 to 1 and tissues such as skin with high values (e.g., 0.9) permit little plasma-protein escape. Further details concerning the diffusion and Starling equations can be found in standard textbooks of Physiology and in several excellent reviews [12–16].

Permeability as understood by vascular biologists

In contrast to physiologists, vascular biologists have used the term vascular permeability in a less restrictive sense. Rather than being concerned with the permeability of a single cannulated microvessel, they have sought to measure the net amount of a solute, typically a macromolecule such as plasma albumin, that has crossed a vascular bed and accumulated in the interstitium in response to a vascular permeabilizing agent or at a site of pathological angiogenesis. Generally speaking, the vessels involved are not of
a single type, and the measurements made combine together all of the factors, both intrinsic properties of the blood vessels as well as extrinsic properties such as blood flow, that regulate extravasation.

To obtain this type of information, they have generally used the Miles assay or one of its variants [17–19]. Typically, a dye such as Evan’s blue that binds noncovalently to albumin is injected intravenously and its accumulation is measured at some later time at a skin test site (Fig. 1), in a tumor, or in other tissues of interest. Permeability is defined as the amount of albumin–dye complex that is present at some time (often 30 min) after Evan’s blue injection. The intensity of local bluing observed visually provides sufficient information for some purposes. For example, local bluing in guinea pig skin was used to evaluate column fractions in the original purification of vascular permeability factor/vascular endothelial growth factor (VPF/VEGF, VEGF-A) [19]. However, quantitative measurements can be made by extracting the dye from tissues and measuring it spectrophotometrically [20]. A limitation of the Miles assay, whether permeability is assessed visually or by quantitative measurement, is that it does not distinguish between dye that has extravasated from that present within the vasculature. However, serious error does not result when intravascular volumes are small relative to the amounts of dye that have leaked, for example, at skin test sites injected with column fractions containing different amounts of VPF/VEGF. Another limitation is that the Miles assay measures net accumulation of dye–albumin complex over a period of time and return of extravasated molecules to the circulation, either by way of capillaries or lymphatics, is not considered. Despite these limitations the Miles assay has provided much useful information.

However, in tumors and in other examples of pathological angiogenesis, the vasculature undergoes dramatic changes and is not comparable to that of adjacent normal control tissues. In some instances it is important to measure both the content of tracer within blood vessels and that which has extravasated. This can be accomplished using a dual isotope approach [20–22]. Operationally, $^{125}$I-albumin is injected i.v. into a mouse at time zero. After 25 min, a second i.v. injection is administered, this time of $^{131}$I-albumin. After 5 min, at time 30 min, blood is collected, animals are euthanized and tissues of interest are harvested, weighed, and subjected to gamma counting. The following equations are used to calculate intravascular plasma volume ($V_p$) and the albumin leakage rate ($LR$):

$$A_{131} = C_{p131} \times V_p + LR \times C_{p131} \times 5$$

$$A_{125} = C_{p125} \times V_p + LR \times C_{p125} \times 30$$

$$LR = 1/25 \times (A_{125}/C_{p125} - A_{131}/C_{p131})$$

$$V_p = 1/5 \times (6 \times A_{131}/C_{p131} - A_{125}/C_{p125})$$

$$A = C_p \times V_p + LR \times C_p \times t$$

where $A$ is total tissue radioactivity ($\mu$Ci/g) of $^{125}$I-albumin or $^{131}$I-albumin; $C_p$ is concentration of radioactive tracer in plasma ($\mu$Ci/$\mu$l); $V_p$ is volume of plasma in tissue ($\mu$l/g); $LR$ is the leakage rate from plasma into tissue expressed as $\mu$l/min-g and is equivalent to the permeability–surface area product; and $t$ is time elapsed since injection of tracer (min).

An underlying assumption of this method is that even in the case of highly leaky blood vessels only negligible amounts of $^{131}$I-albumin will have had time to extravasate at 5 min after injection. Therefore, the $^{131}$I-albumin value at 5 min provides a quantitative measure of intravascular volume whereas the $^{125}$I-albumin value provides a measure of the sum of both intravascular and extravascular albumin. Extravasated albumin (i.e., the volume of plasma extravasated in 25 min) can then be determined by subtracting the 5 min value from the 30 min value. This method has the disadvantages of using a strong, short-lived gamma emitter ($^{131}$I) and of not permitting visual inspection of tracer leakage as when Evan’s blue dye is used as tracer. To circumvent these limitations we recently modified the method by substituting Evan’s blue dye (hence plasma albumin) for the first tracer (30 min time point) and using $^{125}$I-albumin for the second (5 min time point).
In vitro permeability assays or in vivo veritas?

The assays described above measure permeability in living animals. However, a number of groups have used in vitro assays to measure the flux of small or large molecules across lawns of confluent endothelial cells cultured on membrane filters in transwell chambers [5, 10, 23–26]. These assays are appealing in that they are relatively easy to perform and avoid the complexities of studies in living animals. However, in our view they suffer from severe limitations. Confluent-cultured endothelial cell monolayers, whether isolated from large or small vessels, are generally leakier than the normal blood vessel wall in vivo, perhaps because pericytes or smooth muscle cells that normally modify endothelial cell behavior are missing. Also, cultured endothelial cells generally have relatively few cytoplasmic vesicles and vacuoles, structures which are numerous in these same cells in vivo and provide the means by which solutes, and especially proteins, cross capillary and venular endothelium in vivo. Attempts to restore these vesicles have only been achieved in cultured endothelium under specialized conditions that are not easily amenable to permeability assays [27, 28]. Cultured endothelial cells are extremely flattened cells that do not resemble, for example, the cuboidal venular endothelium that is responsive to permeability agents such as VEGF-A or histamine in vivo. Finally, the kinetics of leakage in response to agents such as VEGF-A differ markedly in vivo and in cultured endothelium. In vivo, leakage in response to a single exposure to VEGF-A begins within a minute and is largely complete by ~30 min. However, increased permeability develops much more slowly in cultured endothelium and often peaks over a period of hours, suggesting that the permeability observed may reflect, at least in part, a loosening of intercellular connections as endothelial cell are stimulated to migrate by VEGF-A. In sum, current in vitro assays do not mimic the basal vascular permeability or acute vascular hyperpermeability observed in vivo, but may provide a model for measuring the chronic vascular hyperpermeability characteristic of pathological angiogenesis as found in tumors, healing wounds, and chronic inflammation (see below).

Basal vascular permeability (BVP), acute vascular hyperpermeability (AVH), and the chronic vascular hyperpermeability (CVH) of pathological angiogenesis

As was already noted, low levels of vascular permeability to plasma proteins are essential for the health of normal tissues and these levels may vary considerably at different times in different organs and tissues in response to different physiological stimuli, e.g., exercise. However, it is important to distinguish between the basal permeability levels of normal tissues and the greatly increased levels of plasma protein extravasation that occur in pathology. These hyperpermeable states may be acute or chronic and differ from each other and from basal levels of permeability with respect to the vessels that leak, the composition of the extravasate, and the anatomic pathways that solutes follow in crossing vascular endothelium. Each of the three types of permeability will now be discussed in turn.

**Basal vascular permeability (BVP)**

Molecular exchange in normal tissues takes place primarily in capillaries. Indeed, it may be stated that the primary function of several major organs (heart, lungs, kidneys) and of larger blood vessels (arteries, arterioles, veins, venules) is to supply the capillaries, and thus the tissues, with nutrients and to clear waste products. The molecules exchanged consist largely of gases (O$_2$ and CO$_2$), water, small molecules such as salts and sugars, and only small amounts of plasma proteins. The process is driven largely by diffusion. The extent of BVP varies considerably in different normal tissues and is subject to substantial change in response to changes in hydrostatic pressure, opening of closed vessels, surface area available for exchange, blood flow, etc.

How do plasma water and solutes of different size traverse capillaries? As noted above, physiologists have likened capillary endothelium to a thin, passive barrier penetrated by pores of varying size. These putative pores were recognized to be too small to be visualized by light microscopy. Therefore, there was great excitement that electron microscopy, as it became available in the 1950s, would be able to visualize the pores. But these expectations were not immediately realized. No “pores” as such were found in normal capillary endothelium. Nonetheless, it was not difficult to explain the transport pathways followed by small molecules. Water and lipophilic solutes (e.g., gases such as O$_2$ and CO$_2$) are able to diffuse through endothelial cells; they also pass readily through inter-endothelial cell junctions and through endothelial fenestrae. Small lipophilic molecules can also dissolve in endothelial cell membranes and so pass from the vascular lumen to the interstitium. However, none of these routes provided a satisfactory explanation for the passage of large molecules. Small proteins such as horseradish peroxidase can pass

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1 Fenestrae are greatly thinned (70–150-nm diameter) zones of microvascular endothelium that can be induced by VEGF-A [60]. They are found in small numbers in many types of vascular endothelium and are especially numerous in specialized vascular beds that supply tissues that secrete protein hormones. They are induced in other types of vascular endothelium by VEGF-A [60]. Fenestrae are closed by a thin diaphragm, similar structurally to the diaphragms closing the stomata found in caveolae and VVOs [29, 34].
through inter-endothelial cell junctions, but do so at rates that are much slower than their entry into tissues [29, 30]. Further, at a MW of 44 kD, HRP is significantly smaller than the smallest plasma proteins such as albumin (MW 69 kD) and therefore does not provide an ideal model for plasma-protein leakage.

A solution to the problem of plasma-protein extravasation into normal tissues was offered by George Palade who observed that capillary endothelium contained large numbers of small (~70-nm diameter) vesicles [31–33]. He named these plasmallemmal vesicles and they are now more commonly referred to as caveolae (Fig. 2a, b). The majority of caveolae are found connected to the luminal and abluminal plasma membranes by means of stomata that are generally closed by thin diaphragms. Little is known about the composition of these diaphragms other than that they contain a unique protein, PV–1, and likely sulfated proteoglycans [34]. Palade postulated that caveolae shuttled across capillary endothelium carrying cargoes of plasma fluid and proteins and this was subsequently demonstrated experimentally with tracers (reviewed in [29]). Thus it seemed that the large pores postulated by physiologists were not pores at all but shuttling caveolae and that transport of large molecules across capillaries was anything but passive. This concept stood the test of time until quite recently when it was found that caveolin-1 null mice that lack capillary endothelial caveolae altogether actually exhibit increased permeability to albumin [35, 36]. More will be said about this later.

**Acute vascular hyperpermeability (AVH)**

A rapid increase in vascular permeability occurs when the microvasculature is exposed acutely to any of a number of vascular permeabilizing factors, e.g., VEGF-A, histamine, serotonin, PAF, etc. Some of these agents (e.g., histamine, serotonin, VEGF-A) are normally stored in tissue mast cells [37–39] and so may be released by agents that cause mast cell degranulation, e.g., allergy, insect bites, etc. Single exposure to any of these permeability factors results in a rapid but self-limited (complete by 20–30 min) influx of plasma into the tissues. Not only is the quantity of extravasated fluid greatly increased above that found in BVP but its composition is greatly changed. As already noted, the fluid passing from the circulation into normal tissues under basal conditions is a plasma filtrate, i.e., a fluid consisting largely of water and small solutes but containing very little plasma protein. However, the fluid that extravasates in AVH is rich in plasma proteins, approaching the levels found in plasma, and is referred to as an *exudate*. Among the plasma proteins that extravasate are fibrinogen and various members of the blood clotting cascade. When these come into contact with tissue factor, a protein that is normally expressed by many interstitial cells, the clotting system is activated and the exudate clots to deposit fibrin [40, 41]. Fibrin forms a gel that traps water and other solutes, restraining their clearance by lymphatics or capillaries and resulting in tissue swelling (edema). Fibrin in tissues has other functions that are discussed below. However, as long as the permeability stimulus is not continuous, the deposited fibrin is rapidly degraded without further consequences.

AVH also differs from BVP in that, as Guido Majno demonstrated, the vascular leakage takes place not from capillaries but from post-capillary venules, highly specific vessels just downstream of capillaries [42, 43]. Whereas capillaries have a flattened endothelium, venules are lined by a much taller, cuboidal endothelium. Majno also proposed a mechanism of protein leakage, namely that histamine and other vascular permeabilizing agents induced endothelial cells to contract and pull apart to form intercellular (paracellular) gaps of sufficient size to permit plasma-protein extravasation.

More recently, a structure was discovered in venular endothelium, the vesiculo-vacuolar organelle (VVO), that offers an alternative, trans-endothelial cell route for plasma extravasation in response to permeability factors [44–48]. VVOs are grape-like clusters comprised of hundreds of uncoated, cytoplasmic vesicles and vacuoles that together
form an organelle that traverses venular endothelial cytoplasm from lumen to albumen (Figs. 3(a, b), 4a). VVOs often extend to inter-endothelial cell interfaces and their individual vesicles (unlike caveolae) commonly open to the inter-endothelial cell cleft. The vesicles and vacuoles comprising VVOs vary in size from those the size of caveolae to vacuoles with volumes as much as 10-fold larger [49]. These vesicles and vacuoles are linked to each other and to the luminal and abluminal plasma membranes by stomata that are normally closed by thin diaphragms that appear similar to those found in caveolae. We conjectured some years ago that VVOs formed from the linking together of individual caveolae and that larger vesicles and vacuoles resulted from the fusion of two or more caveolae-sized vesicles [49]. Evidence for this was that the smallest VVO vesicles were indistinguishable structurally from caveolae and larger vesicles and vacuoles have volumes that do not fall on a continuum but have a modal distribution, i.e., occur as multiples of the volume of caveolae, the unit vesicle, up to 10-mers. However, VVO vesicles and vacuoles only stain irregularly for caveolin (unpublished data), a protein that is demonstrable by electron microscopic immunocytochemistry in nearly all plasma membrane-connected caveolae. Also, whereas the capillaries in caveolin-1 null mice lack caveolae altogether [36], VVOs are present in normal numbers in the venular endothelium of these mice (unpublished data). Whether VVOs somehow take the place of caveolae in caveolin-1 null mice and thereby contribute to the increased permeability observed in these animals needs to be investigated.

Although very little is known about the mechanisms of VVO function, it is clear that, upon exposure to histamine, VEGF-A, etc., macromolecular tracers such as ferritin pass through a sequence of inter-connected VVO vesicles and vacuoles from the vascular lumen to the albumen (Fig. 4b). It seems that vascular permeability inducing agents cause the diaphragms interconnecting vesicles and vacuoles to open, thereby providing a transcellular pathway for plasma and plasma-protein extravasation. The underlying mechanism could be mechanical, as was the endothelial cell contraction mechanism originally postulated by Majno [43]. If so, the actin–myosin contractions induced by

Fig. 3 Transmission electron micrographs of venules in normal mouse ear skin (a, b) and of a mother vessel (c, d) 3 days after local injection of Ad-VEGF-A164. (a, b) Typical normal venules lined by cuboidal endothelium. The cytoplasm contains prominent vesiculo-vacuolar organelles (VVOs) and is enveloped by a complete coating of pericytes (P). R, red blood cell. (c, d) MV are greatly enlarged vessels that are characterized by extensive endothelial cell thinning; striking reduction in VVOs and other cytoplasmic vesicles; prominent nuclei that project into the vascular lumen; frequent mitotic figures (arrows, c); endothelial cell bridging with the formation of multiple lumens (L, d); and pericyte (P) detachment in (c). The mother vessel lumen (c) is packed with red blood cells, indicative of extensive plasma extravasation. Inset. The normal venule depicted in a is reproduced in c at the same magnification as the mother vessel to illustrate differences in relative size of normal venules and MV. Scale bars: (a, b) 1 µm; (c, d) 5 µm

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function that lead to the chronic hyperpermeability of exposure results in profound changes in venular structure and self-limited hyperpermeability of normal venules, chronic Whereas acute exposure to VEGF-A results in immediate but

Chronic vascular hyperpermeability (CVH)

Whereas acute exposure to VEGF-A results in immediate but self-limited hyperpermeability of normal venules, chronic exposure results in profound changes in venular structure and function that lead to the chronic hyperpermeability of pathological angiogenesis as found in tumors, healing wounds, and chronic inflammatory diseases such as rheumatoid arthritis, psoriasis, cellular immunity, etc. [1, 2, 51]. As in AVH, the fluid that extravasates is an exudate that approaches the overall composition of plasma. In tumors fluid accumulation is generally associated with increased interstitial pressure [52]; this increased pressure results from persistent vascular hyperpermeability, clotting of the exudate with deposition of a fluid-trapping fibrin gel, inadequate lymphatic drainage, and the restraints imposed by surrounding tissues that together limit fluid dissipation. However, these restraints are nearly absent when tumors grow in or around body cavities such as the peritoneum where massive amounts of ascites fluid (many liters) can accumulate.

In contrast to BVP and AVH, fluid leakage in CVH does not take place from any type of normal blood vessel. Instead, whether in tumors or wounds, the blood vessels that leak are newly formed, highly abnormal angiogenic blood vessels; these are primarily mother vessels (MV), and also, to a lesser extent, glomeruloid microvascular proliferations (GMP) that form from MV [20, 53–57] (Figs. 3c, d, 4c, 5). Mother Vessels are greatly enlarged sinusoids that arise from preexisting normal venules by a process that involves pericyte detachment, vascular basal lamina degradation, and a 4–5-fold increase in lumen size that is accompanied by extensive endothelial cell thinning. Poiseille’s law indicates that blood flow is proportional to the fourth power of the vascular radius. Nonetheless, MV exhibit sluggish blood flow because of their hyperpermeability to plasma which results in a striking increase in hematocrit (Fig. 3c).

As expected, the protein-rich exudates in CVH interact with tissue factor to trigger the clotting system and deposit fibrin [40, 41]. Tissue factor is expressed on many tumor cells as well as host interstitial cells and is induced in endothelial cells by VEGF-A [58]. In addition to its fluid trapping properties, fibrin also has a number of other properties when it persists over time as in tumors and healing wounds. It provides a pro-angiogenic provisional stroma that induces and is later replaced by the ingrowth of new blood vessels and fibroblasts and the laying down of mature fibro-vascular stroma [2, 17, 59]. Fibrin interacts with integrins expressed by multiple cell types and so supports the migration of tumor cells as well as host mesenchymal cells (endothelial cells, pericytes, fibroblasts) and inflammatory cells (neutrophils, monocytes). Fibrin

Although careful measurements have not been made, it is unlikely that extensive vascular permeability accompanies the angiogenesis of normal development. At least in later stages of embryonic growth and post-natally, the developing blood vessels exhibit the structure of normal adult vessels and do not resemble the chronically permeable MV found in pathological angiogenesis.
also sequesters growth factors, protecting them from degradation, and induces the expression of proangiogenic molecules such as IL-8 and tissue factor. Fragment E, a fibrin breakdown product, is directly pro-angiogenic (reviewed in [1, 58]).

Macromolecules such as ferritin extravasate from MV and GMP largely by a transcellular route [20]. As noted above, MV develop from normal venules by a process that involves extensive vascular enlargement with consequent endothelial cell thinning, processes that are thought to be facilitated, at least in part, by a transfer of VVO membranes to the plasma membrane [20]. As a result, MV, as well as the GMP that derive from MV, contain many fewer and less complex VVOs than normal venular endothelium. However, the path length for molecular extravasation is greatly shortened as tracers such as ferritin need to pass through only a few, often only one or two, vesicles or vacuoles to reach the ablumen (Fig. 3(c, d), 4c, 5b). Macromolecules also extravasate through fenestrae that are present in both MV and GMP [49] (Figs. 4c, 5c). Pores of the type that have been described in AVH have also been found in the endothelial cells of blood vessels.

Table 1 Decreased (↓↓), increased (↑↑), or unchanged (↔↔) basal, acute, or chronic vascular permeability in various engineered mice

| Basal | ↓↓ | Caveolin-1 null [36]; [35]; eNOS null [66]; endothelial cell specific myrAkt TG [67]; PI3K K14 TG [68]; VEGF-A<sup>164</sup> K14 TG [69]; VEGF-A<sup>120</sup> K14 TG [70]; collagen XVIII null [71] |
|-------|----|-----------------------------------------------|
|       | ↑↑ | eNOS null [72]; Akt-1 null [64, 73, 74]; TSP-1 K14 TG [75]; TSP-2 null [76]; β3 integrin null [77]; HIF-1α K14 TG [78]; |
|       | ↔↔ | eNOS null [72]; Akt-1 null [64, 73, 74]; TSP-1 K14 TG [75]; TSP-2 null [76]; β3 integrin null [77]; HIF-1α K14 TG [78]; |
| Acute, VEGF-A-mediated | ↓↓ | eNOS null [79]; endothelial cell specific caveolin-1 TG [80]; Akt-1 null [73]; Src and Yes null [81]; angiotensin II type 1 receptor null [82]; PI3K null [83, 84]; Ang-1 K14 TG [69]; sNRP-1 K14 TG [85]; ESAM null [86]; β5 integrin null [87]; |
|       | ↑↑ | β3 integrin null [77]; |
|       | ↔↔ | iNOS null [79]; endothelial specific myrAkt endothelial cell TG [67]; Fyn null [81]; collagen XVIII null [71]; |
| Chronic, VEGF-A/tumor mediated | ↓↓ | eNOS null [79]; caveolin-1 null [88, 89]; endothelial cell-specific cav-1 TG [80]; Akt-1 null [73]; PI3K null [84]; |
|       | ↑↑ | β3 integrin null and β3/β5 integrin double null [90]; caveolin-1 null [91, 92]; |
supplying tumors [43, 46, 60] (Fig. 4c). As noted earlier, such openings have often been called intercellular. However, careful 3D reconstructions of serial electron microscopic sections have shown that many pores induced by vascular permeabilizing agents are in fact transcellular pores that pass through endothelial cell cytoplasm [48, 50].

Molecular and genetic events that regulate vascular permeability

This review has shown that vascular permeability, far from being a single, well-defined entity, is instead an extremely complex process that in different settings, involves distinctly different types of blood vessels and makes use of different anatomic pathways. Further, whereas the fluid extravasating in BVH is a plasma filtrate consisting almost entirely of water and small solutes, that extravasating in AVH and CVH, is a protein-rich exudate. Agents such as VEGF-A have long been known to induce AVH and CVH, but, apart from hemodynamic factors, much less is known about the molecular events that are responsible for the normal permeability of BVP. Even less is known about the molecules that are involved in regulating permeability, though this is changing rapidly. In Table 1 we have listed as many of the published gene products of which we are aware that have been implicated in vascular permeability. Some of these molecules have long been known to have roles in permeability whereas others have only recently been recognized to have such a role. However, the signaling pathways by which even such well-studied molecules as eNOS and caveolin-1 act to induce permeability are poorly understood. Almost nothing is known about the molecular mechanisms that regulate such critical events as caveolar shuttling, the opening of VVO diaphragms, the formation of fenestrae, changes in endothelial cell junctions, etc. [61–63]. We have attempted to catalog the molecules in Table 1, as far as is possible with existing knowledge, under the headings of BVP, AVH, and CVH. Some of these molecules are clearly involved in all three types of permeability whereas others apparently are not. The molecular mechanisms that govern each of the different types of permeability may well be different and are a subject for further research. As an example, Phung et al. found that, unlike the AVH induced by VEGF-A, the CVH found in mice over-expressing myr-Akt in vascular endothelium was not regulated by eNOS [64].

Finally, just as the angiogenic response induced by VEGF-A differs significantly in different mouse strains [65], it is likely that the permeability response, both basal and that induced by permeability factors, will also differ in mice with different genetic backgrounds, though this has not as yet been investigated in any systematic manner.

Conclusions

This review has provided a framework for measuring vascular permeability. It has also demonstrated that vascular permeability needs to be considered in at least three distinctly different settings: BVP, AVH and CVH. These distinctions are important as it is likely that both common and different molecular mechanisms are involved in each. Future work will need to focus on the molecular mechanisms by which the molecules in Table 1, and likely others yet to be discovered, act to regulate permeability in each of the three settings.

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