3D vena contracta area in degenerative mitral regurgitation: cross-platform comparison in a single patient

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Quantification of degenerative mitral regurgitation (MR) by two-dimensional (2D) transthoracic echocardiography (TTE) and transesophageal echocardiography (TEE) is challenging. Eccentric, obliquely oriented regurgitant jets limit inter-observer and intra-observer consistency. In recent years, with increasingly sophisticated three-dimensional (3D) TTE and TEE systems that enable single-beat 3D color acquisition, 3D vena contracta area (VCA) has emerged as an attractive indicator of MR severity. It overcomes geometric assumptions in 2D techniques and can be acquired in a single cardiac cycle, which is a major benefit in atrial fibrillation. However, most studies of 3D VCA were performed on the Philips TEE platform.1-3 The performance of the technique on GE systems and on 3D TTE is unexplored. We report 3D VCA measurements in a case of severe degenerative MR on 3D TTE (4V-D transducer, Vivid E95, GE Vingmed Ultrasound, Horten, Norway), and 3D TEE performed on GE (6VT-D transducer, Vivid E95, GE Vingmed Ultrasound, Horten, Norway) and Philips (X7-2t transducer, EPIC 7C, Philips Medical Systems, Andover, MA, USA).

A 73-year-old woman presented with acute dyspnea for two days. She had history of well-controlled hypertension and diabetes mellitus. An apical pansystolic murmur was noted. Chest radiograph showed pulmonary edema. Electrocardiogram showed sinus tachycardia. The 2D TTE (GE) demonstrated normal left ventricular ejection fraction and posterior mitral leaflet flail was performed. Effective regurgitant orifice area (EROA) was 0.8 cm² by proximal isovelocity surface area (PISA) method. Single-beat color Doppler of MR was acquired at apical window on 3D TTE. Image quality was suboptimal at parasternal window. Aliasing velocity was set at default of 66 cm/s. Variance map was turned on to minimize color mosaic on image analysis. Field of view was adjusted to achieve frame rate of 15–20 frames/s. Offline multiplane reformatting of acquired image at peak systole enabled double-oblique correction of jet orientation and identification of plane perpendicular to jet direction (Figure 1). 3D VCA was measured at 1.12 cm² by planimetry of green area on variance map. 3D TEE (Vivid E95, GE) was performed four days later under conscious sedation for preoperative planning. P2 flail due to chordal rupture was confirmed (Figure 2). Single-beat color Doppler was acquired and postprocessed offline in a similar fashion. 3D VCA was planimetrically measured at 1.21 cm² (Figure 3).

Figure 1 The vena contracta area measures 1.12 cm² on multiplanar reconstruction of 3D transthoracic echocardiography (Vivid E95, GE) at peak systole. The reconstruction plane is perpendicular to the narrowest neck of color flow on two orthogonal planes, which defines the vena contracta. Aliasing velocity is set at 66 cm/s with variance map enabled.
The patient received open mitral valve repair two weeks after admission during which another 3D TEE (EPIC 7C, Philips) was performed after induction of general anesthesia but before sternotomy. Aliasing velocity was set at 53.9 cm/s; frame rate was adjusted to 15–20 frames/s. Online postprocessing identified a 3D VCA of 1.35 cm$^2$ by planimetry of aliased area (Figure 4). Notably, variance map option was not available in 3D color acquisition on this version of firmware. Intraoperatively P2 flail and chordal rupture was repaired with triangular resection and mitral annuloplasty leaving minimal MR. The patient remained asymptomatic three months postoperatively.

Our case shows that 3D VCA is highly consistent across platforms (TTE vs. TEE) and vendors (GE vs. Philips), while PISA significantly underestimated EROA compared to 3D VCA. PISA assumes a circular regurgitant orifice, which is rarely the case in eccentric, degenerative MR. For example, the 3D VCA depicts an elliptical regurgitant orifice in this patient. Depending on how the orifice is transected, PISA may underestimate or overestimate the EROA. Several technical details are important to observe in the application of 3D VCA technique. Firstly, single-beat acquisition is preferred. Stitch artifacts with multi-beat acquisition may distort the color map and introduce error in measurement. Secondly, the field of view should be as small as possible to maximize frame rate, while as large as necessary to include the entire regurgitant orifice. Any truncation of the regurgitant orifice invalidates the result. Last but not the least, aliasing velocity should be set at 55–66 cm/s, which is the default on most systems, and variance map should be turned on if available. We found that higher aliasing velocities deflate the measured VCA, whereas lower values inflate. In addition, speckles of color may intermix at the regurgitant orifice as flow becomes turbulent. It causes confusion to delineation of VCA. Variance map greatly simplifies the situation by dichotomizing the color flow into areas of turbulence and areas without. Turbulence being a hallmark of flow convergence at vena contracta helps to exclude areas of “color blooming” that would otherwise exaggerate the measured VCA.

In summary, we showed the value of 3D VCA as a feasible, robust measure of degenerative MR across different platforms (TTE vs. TEE) and vendors (GE vs. Philips) in a single patient under different loading conditions ranging from fully conscious to under general anesthesia.
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