Inflammatory bowel diseases (IBDs) are a set of complex and debilitating diseases for which there is no satisfactory treatment. Recent studies have shown that small peptides show promise for reducing inflammation in models of IBD. However, these small peptides are likely to be unstable and rapidly cleared from the circulation, and therefore, if not modified for better stability, represent non-viable drug leads. We hypothesized that improving the stability of these peptides by grafting them into a stable cyclic peptide scaffold may enhance their therapeutic potential. Using this approach, we have designed a novel cyclic peptide that comprises a small bioactive peptide from the annexin A1 protein grafted into a sunflower trypsin inhibitor cyclic scaffold. We used native chemical ligation to synthesize the grafted cyclic peptide. This engineered cyclic peptide maintained the overall fold of the naturally occurring cyclic peptide, was more effective at reducing inflammation in a mouse model of acute colitis than the bioactive peptide alone, and showed enhanced stability in human serum. Our findings suggest that the use of cyclic peptides as structural backbones offers a promising approach for the treatment of IBD and potentially other chronic inflammatory conditions.

Inflammatory bowel diseases (IBDs) are a set of chronic inflammatory disorders of the gastrointestinal tract; the two major forms are ulcerative colitis and Crohn’s disease. Although there are several medications on the market for IBD, they generally only provide temporary relief, and 70% of IBD patients require surgical intervention. Because the current treatments are not satisfactory, new drug leads are being sought from a range of sources, including small molecules from plants and bioactive regions of larger proteins.

Intriguingly, several small peptides, some comprising only three residues, have been shown to be effective in the treatment of experimental colitis in mice. One example is a tripeptide (MC-12) derived from annexin A1, a calcium-dependent phospholipid-binding, anti-inflammatory protein. Annexin A1 mediates expression of cytokines such as TNF-α, IL-6, and IL-10. It is required for the inhibition of NF-κB activity by anti-inflammatory drugs and has recently been shown to be a potential biomarker of therapeutic efficacy for IBD. The N-terminal region of annexin A1 comprising residues 2–26 has been well studied and appears to have the same biological effects as the full-length protein. Analysis of a series of peptides based on the N-terminal sequence of annexin A1 showed that MC-12 (Ac-Gln-Ala-Trp) was the most potent inhibitor of NF-κB activity in SW480 cells.

Small peptides such as MC-12 are likely to be unstable and not viable drug leads, supported by the finding that high doses (25 mg/kg) of MC-12 were required to elicit an in vivo response in mouse colitis models, and it was more effective when injected compared with oral administration. Improving the stability of MC-12 and related peptides may enhance their therapeutic potential.

A range of approaches has been used to improve the stability of peptides, including backbone cyclization, and grafting into cyclic peptide scaffolds. Both approaches are based on the inherent stability observed for naturally occurring cyclic peptides such as cyclosporine, an 11-residue cyclic peptide, used clinically as an immunosuppressant agent. Sunflower trypsin inhibitor 1 (SFTI-1) is an example of a cyclic peptide that has proven useful in grafting studies. SFTI-1 was originally isolated from the seeds of sunflowers (Helianthus annuus), contains 14 residues and is one of the most potent trypsin inhibitors known. The structure comprises two short antiparallel β-strands that are linked by a single disulfide bond. The two loops formed by the cyclic backbone and disulfide bond are termed the “binding” loop, which contains the active-site lysine residue for binding to trypsin, and the “cyclization” loop, which contains the residues involved in the backbone cyclization. In addition to the cyclic backbone and disulfide bond, SFTI-1 contains a network of disulfide bonds that are linked by a single disulfide bond.
of hydrogen bonds, all of which make the peptide highly stable (19). Amino acid substitutions are structurally well tolerated, and the protease inhibitory activity can be removed by mutation of the active-site lysine residue from the binding loop (20). The stability and tolerance to sequence changes makes SFTI-1 a promising peptide drug scaffold (19, 21, 22). Engineered forms of SFTI-1 have been developed as inhibitors of the serine proteases KLK4, KLK5, and KLK7, which are possible targets for cancer treatment (21, 23) as well as in the development of angiogenic agents (22), anti-angiogenic agents (24), and matriptase inhibitors (25).

Here we show that grafting the tripeptide MC-12 into the SFTI-1 scaffold improves its therapeutic efficacy in a murine model of chemically induced acute colitis while also improving its in vitro stability. A schematic representation of the grafting approach is shown in Fig. 1, highlighting the helical structure of MC-12 in annexin A1. A range of peptides was synthesized to explore the importance of the cyclic backbone and the loop into which the sequence was grafted.

Results

Peptide design and synthesis

The tripeptide MC-12 was grafted into the SFTI-1 cyclic scaffold with the aim of improving its stability and potency. MC-12 was grafted into the binding loop of SFTI-1, as this resulted in removal of the P1 lysine residue. Acyclic versions of SFTI-1 incorporating the MC-12 sequence were also designed to examine the influence of the cyclic backbone and loop-grafted on structure and activity. Ac2–26 was also synthesized using Fmoc chemistry to provide additional insight into the structure function relationships of the MC-12 sequence. The sequences of the synthetic peptides are shown in Fig. 2.

Structural analysis using NMR spectroscopy

The structures of all the peptides were analyzed using NMR spectroscopy. In general, the peptides displayed significant dispersion in the amide region and a single set of resonances for each residue, consistent with peptides containing β-sheet structure and one well defined conformation. By contrast, lin-MC12(p) had significant overlap in the amide region, which prevented assignment of the resonances. With the exception of lin-MC12(p), two-dimensional spectra (TOCSY and NOESY) allowed assignment of the resonances, and the secondary chemical shifts (secondary shifts) were determined by subtracting random coil chemical shifts (26) from the αH chemical shifts. A comparison of the secondary shifts is shown in Fig. 3. The secondary shifts were similar between cyc-MC12 and lin-MC12(n), but lin-MC12(l2) had significantly different shifts for the cysteine residues compared with the other two peptides. The cysteine residues form part of the β-hairpin in the native peptide and consequently had downfield-shifted α protons. The lack of downfield-shifted α protons for the cysteine residues in lin-MC12(l2) suggests that the overall fold differs from the native peptide.

Despite the similarities in secondary shifts between cyc-MC12 and lin-MC12(n), analysis of the amide exchange rates shows a significant difference as shown in Table 1. The exchange rates for lin-MC12(n) were higher than those observed for cyc-MC12, indicating that the overall structural stability had been decreased.

The three-dimensional structures of cyc-MC12 and Ac2–26 were determined using the program CYANA based on distance restraints from the NOESY spectrum and angle restraints derived from TALOS+. The 20 lowest energy structures were chosen to represent the structures of cyc-MC12 and Ac2–26. Cyc-MC12 had a well defined structure, including the loop containing the grafted residues as shown in Fig. 4. The structure overlapped with the backbone atoms of SFTI-1 with a root mean square deviation of 1.32 Å, highlighting the similarity between the two peptides. The structure statistics are provided as supplemental Table 1. The structures of Ac2–26 are most well defined over the first 13 residues with a root mean square deviation of 0.08 Å over the backbone atoms as shown in Fig. 5. An α-helix is present from residues 7–10, with residues 9 and 10 corresponding to the Gln and Ala of MC-12. A 3_10 helix is also present between residues 15–17. The structure statistics are provided as supplemental Table 2.

2,4,6-Trinitrobenzenesulfonic acid (TNBS) mouse model

The TNBS-induced murine colitis model was used to test the biological activities of all peptides. Mice were either left untreated (naïve) or were treated with peptide 5 h before administration of TNBS. On day 3 of the experiment, all mice were euthanized by gas asphyxiation and examined. Mice treated with TNBS alone lost weight within 1 day of TNBS administration and continued to lose weight until day three. Initial experiments used 1 mg/kg body weight dosage for cyc-MC12(n), but lin-MC12(l2) had significantly different shifts for the cysteine residues compared with the other two peptides. The cysteine residues form part of the β-hairpin in the native peptide and consequently had downfield-shifted α protons. The lack of downfield-shifted α protons for the cysteine residues in lin-MC12(l2) suggests that the overall fold differs from the native peptide.

Despite the similarities in secondary shifts between cyc-MC12 and lin-MC12(n), analysis of the amide exchange rates shows a significant difference as shown in Table 1. The exchange rates for lin-MC12(n) were higher than those observed for cyc-MC12, indicating that the overall structural stability had been decreased.

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Figure 3. Secondary shift analysis of peptides. The secondary shifts for SFTI-1 are shown in red, cyc-MC12 in blue, lin-MC12(n) in cyan, and lin-MC12(2) in yellow. The secondary shifts were calculated by subtracting the random coil shifts (26) from the Δδ shift. The overall shifts are similar for all peptides with the exception of lin-MC12(2), where the shifts for the cysteine residues (residues 3 and 11) differ significantly from the other peptides.

Table 1
Experimental amide exchange rates (kex, min⁻¹) for cyc-MC12 and lin-MC12 (n)

| Residue | Cyc-MC12 | Lin-MC12(n) |
|---------|----------|-------------|
| Gly-1   | 2.2      | ×10⁻³       |
| Cys-3   | 0.56     | 61          |
| Thr-4   | 1.2      |             |
| Ala-6   | 1.8      |             |
| Trp-7   | 0.37     | 13          |
| Ile-10  | 3.5      | 69          |
| Cys-11  | 0.53     | 33          |
| Phe-12  |          |             |

MC12, but only partial protection in the TNBS model was observed (results not shown), so subsequent experiments used 3 mg/kg. Mice that were treated with 60 μg (3 mg/kg) of cyc-MC12 before administration of TNBS displayed significantly reduced weight loss at day 3, whereas all other peptides tested, including the linear form of the MC-12 peptide, had no significant effect (Fig. 6A). Consistent with enhanced protection against TNBS-induced colitis, cyc-MC12-treated mice had visibly longer, healthier looking colons than untreated control mice administered TNBS (Fig. 6B). The length of the colon in cyc-MC12-treated mice was similar to that of naïve mice (Fig. 6C). Colons were then scored macroscopically by the following parameters: adhesions, bowel wall thickening, mucosal edema, ulceration, necrosis, and colon length (macroscopic score); they demonstrated that cyc-MC12-treated mice displayed a significantly reduced macroscopic score (Fig. 6D). SFTI-1 displayed no protective effect, indicating that this approach might be useful for the design of novel drug leads for the treatment of colitis and other inflammatory diseases.

Serum stability

The stability of the peptides in human serum was assessed over an 8-h period as shown in Fig. 7. MC-12 and annexin A1(2–26) were completely degraded after 8 h. By contrast, cyc-MC12 was stable in human serum over the time course of the experiment. The acyclic peptides were more stable than MC-12 and Ac2–26, but were degraded to ~60% of the initial concentration within the first 3 h of incubation. The lower stability of the linear peptides demonstrates that the disulfide bond alone is not sufficient to confer high stability and that the cyclic backbone enhances the stability of the grafted peptides in human serum.

Discussion

This study broadens the knowledge on grafting bioactive sequences into stable cyclic peptide scaffolds. Grafting MC-12 into the SFTI-1 cyclic scaffold enhances its bioactivity in a mouse model of acute colitis and stability in human serum, indicating that this approach might be useful for the design of novel drug leads for the treatment of colitis and other inflammatory diseases.

Cyc-MC12 had a significant effect on weight loss, macroscopic score, and colon length in the TNBS mouse colitis model. By contrast, MC-12 did not improve weight loss or the macroscopic score relative to the TNBS-treated mice. A significant difference was observed between the colon length of MC-12-treated mice and TNBS-only-treated mice but not to the same extent as cyc-MC12. Both MC-12 and cyc-MC12 were injected into mice at a dose of 3 mg/kg, but MC-12 has a significantly lower molecular weight than cyc-MC12 (MC-12: 445.47 g/mol; cyc-MC12 1570.81 g/mol) corresponding to a higher molar concentration. The original study on MC-12 in colitis required a dose of 25 mg/kg to elicit an influence on macroscopic score and colon length in a TNBS mouse model (18); no effect on weight loss was observed. This improvement in bioactivity of MC-12 in vivo upon grafting in the cyclic scaffold is likely to be related to the significant improvement in stability in serum of cyc-MC12 compared with MC-12.

The three-dimensional structure of cyc-MC12, determined by NMR spectroscopy, is well defined, including the grafted Gln-Ala-Trp sequence. The residues corresponding to MC-12 form a helical structure in the annexin A1 protein (27) as shown in Fig. 1 but do not form a helix when grafted into the cyclic scaffold. This is not surprising given the tightly folded structure of SFTI-1 resulting from the cyclic backbone and cross-bracing of the disulfide bond. Given the well-defined nature of the cyclic peptide, it is unlikely it can change conformation significantly to interact with a binding partner. However, based on the activity observed in the TNBS mouse model, the turn structure induced by grafting into the cyclic scaffold appears to be sufficient to allow binding to the biological target. The biological target for cyc-MC12 is unknown, but the original studies on the MC-12 tripeptide suggested that NF-κB, a central mediator of gastrointestinal inflammation in IBD, might be involved (18, 28). Further study on these peptides is required to elucidate the mechanism of action.
Although the binding partner of MC-12 has not been conclusively shown, our current study provides significant insight into the structure function relationships involved in the anti-inflammatory activity. The importance of the cyclic backbone in SFTI-1 grafting has been highlighted in the current study. Previous studies have shown that the disulfide bond and network of hydrogen bonds are sufficient to maintain the native fold (29). However, in the current study we have shown that although the native fold is maintained in the absence of the cyclic backbone in lin-MC12(n), the bioactivity is not maintained. Cyc-MC12 is structurally more stable than lin-MC12(n) based on the slower amide exchange rates and is more biologically stable in human serum than lin-MC12(n). This lack of stability of lin-MC12(n) might account for the lack of bioactivity in vivo. Interestingly, when the MC-12 peptide is grafted into the SFTI-1 binding loop, without backbone cyclization in lin-MC12(p), the chemical shift analysis indicates that the overall fold of the native peptide is not maintained. This peptide has a large extended N-terminal tail that presumably prevents the native structure from forming.

Further insight into the structure function relationships of MC-12 have come from analysis of Ac2–26. Ac2–26 is effective in a range of anti-inflammatory assays including models of ocular inflammation and asthma at doses of 1 mg/kg (30, 31), but the structure has not been reported. We show here that the N-terminal region, including the MC-12 sequence (residues 9–11), is well defined in contrast to the C-terminal region of the peptide (Fig. 5). Residues 9–11 in Ac2–26 overlay well with the corresponding residues in the full-length annexin A1 protein as shown in Fig. 8, but the adjacent residues in Ac2–26 do not overlay with the full-length protein. The conservation of the native structure of MC-12 in the Ac2–26 peptide suggests there will be less entropic losses upon binding to the biological target and consequently why this tripeptide has previously been shown to be so important in anti-inflammatory activity (13). In the current study we have shown that Ac2–26 is not as effective as cyc-MC12 in the colitis model, and this lower efficacy is likely to be related to the lower biological stability; Ac2–26 is degraded rapidly in human serum.

In summary, the potency and stability of the MC-12 tripeptide was improved by incorporation into the SFTI-1 scaffold. The cyclic backbone is important for structural and biological stability and consequently biological activity. Overall, our results indicate that SFTI-1 is a promising scaffold for the design of novel lead molecules for IBD and other diseases that result from a dysregulated immune system.

**Experimental procedures**

**Peptide synthesis and purification**

Peptides were synthesized using solid-phase peptide synthesis on a Protein Technologies PS3 synthesizer using Fmoc chemistry on a 0.1-mmol scale. Linear peptides were synthesized on 2-chlorotrityl chloride resin. Amino acids (2 eq.) were activated in 0.5M 2-(1H-benzotriazol-1-yl)-1,1,3,3-tetramethyluronium hexafluorophosphate with 10 eq. of dichloromethane. The first amino acid was coupled manually to the resin (Arg was double-coupled). Peptides were cleaved from the resin using trifluoroacetic acid (TFA)/water/triisopropylsilane (95:2.5:2.5) for 2–3 h, precipitated with diethyl ether, dissolved in 50% acetonitrile, 0.05% TFA and subsequently lyophilized. The resulting crude peptides were purified with RP-HPLC on a C-18 preparative column (Phenomenex Jupiter 250 × 21.2 mm) using a 1% gradient of solvent B (solvent A: 0.05% TFA; solvent B: 90% acetonitrile, 0.05% TFA). Peptides were oxidized in 0.1 M ammonium bicarbonate, pH 8–8.5, and purified using RP-HPLC, and the mass was analyzed using MALDI mass spectrometry.

The cyclic peptide was synthesized using native chemical ligation (32) on Dawson Dbz AM resin (100–200 mesh). The Dawson resin was deprotected with 20% piperidine in dimeth-
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ylformamide (DMF) (2 × 5 min washes) and then washed with DMF before the addition of the first residue. Before cleavage of the cyclic peptide, acylation of the Dbz linker was achieved by adding 4-nitrophenylchloroformate in dichloromethane (16 eq, room temperature) to the dry resin under N2 for 1 h. The resin was then washed with DMF.

\[ \text{N, N-Diisopropylethylamine} \text{ (195 eq.) in DMF} \text{ was added for 1 h at room temperature for activation. After activation, the Nbz-peptide was washed with DMF and dried.} \]

Cyclization was carried out in 200 mM 4-mercaptoenylcarboxylic acid and 20 mM tris(2-carboxyethyl)phosphate in 200 mM phosphate buffer at room temperature for 48 h. The cyclic peptide was purified using RP-HPLC on a C-18 semi preparative column (250 × 10 mm Phenomenex Jupiter C18 column), and mass was analyzed on a 5800 MALDI TOF-TOF (SCIEX) mass spectrometer. The cyclic peptide was oxidized using 0.1 M NH4HCO4. The sample was then purified with RP-HPLC and finally analyzed with NMR.

**NMR spectroscopy**

Lyophilized peptides were resuspended to a final concentration of ~0.2 mM in 90% H2O:10% D2O. 2D 1H, 1H TOCSY, 1H, 1H NOESY, 1H, 15N HSQC, and 13C, 1H HSQC spectra were acquired at 290 K using a 600 MHz
AVANCE III NMR spectrometer (Bruker, Karlsruhe, Germany) equipped with a cryogenically cooled probe. All spectra were recorded with an interscan delay of 1 s. NOESY spectra were acquired with mixing times of 200–300 ms, and TOCSY spectra were acquired with isotropic mixing periods of 80 ms. Standard Bruker pulse sequences were used with an excitation sculpting scheme for solvent suppression. Slowly exchanging amide protons were detected by acquiring a series of one-dimensional and TOCSY spectra over a 24-h period after dissolution of the peptides in D$_2$O. Exchange rates were calculated as previously described for comparison of acyclic and cyclic peptides (33).

The 2D NOESY spectra of cyc-MC12 were automatically assigned and an ensemble of structures was calculated using the program CYANA (34). Torsion-angle restraints from TALOS+ were used in the structure calculations. Procheck (35) and Promotif (36) were used to analyze the stereochemical quality of the final structures, which were visualized using MOLMOL (37).

TNBS colitis assay

All animal experiments were conducted in accordance with the James Cook University Animal Ethics Committee-approved guidelines under the project #A2003. Groups of five male C57BL/6 mice were used (5 weeks old). Mice were purchased from the Animal Resources Centre (Perth, Australia) and housed in the animal care facility unit at James Cook University under specific pathogen-free conditions (Cairns). Mice were placed inside plastic cages with unlimited access to food and water.

Mice were divided randomly into 8 groups: naïve, TNBS, cyc-MC12, SFTI-1, lin-MC12(n), lin-MC12(p), MC12, and annexin A1 (2–26). Experimental mice received intraperitoneal injections of peptides at a dosage of 3 mg/kg body weight. The mice were anesthetized before administration of TNBS using mild ketamine/xylazine solution. After anesthesia, each mouse received 100 μl of 5% (w/v) TNBS solution in 60% ethanol by intra-colonic instillation using a 20-gauge soft catheter (Terumo), which was inserted into the colon. Following the procedure, the animals were kept vertical for 30 s. Mice were monitored daily for piloerection, survival, body weight, decreased motor activity, rectal bleeding, and stool consistency. Macroscopic pathology score was calculated for each colon after the mice were culled. Briefly, colons were harvested, opened longitudinally, and washed with sterile phosphate buffer saline then placed under a microscope (Olympus SZ61, 0.67–4.5x). The tissues were assessed for changes in macroscopic appearance and scored for pathological changes as follows: adhesion (0–3), bowel wall thickening (0–3), mucosal edema (0–3), ulceration (0–3), and colon length as described previously (38). All animal experiments were conducted in duplicate to ensure reproducibility of the findings.

Serum stability assay

The stability of the peptides was tested in human male AB plasma (Sigma) using methods previously described (22). Peptides (final concentration of 200 μM) were incubated in serum or PBS at 37 °C, and 40-μl aliquots were taken at 0 h, 3 h, and 8 h. The aliquots of serum were quenched with 40 μl of 20% TFA and incubated for 10 min at 4 °C to precipitate serum proteins. PBS received the same treatment as serum. The samples were then centrifuged at 17,000 × g for 10 min, and 90 μl of supernatant was analyzed by RP-HPLC at a flow rate of 0.3 ml/min using an Phenomenex Jupiter C12 analytical column (150 × 2.00 mm, 4 μm, 90 Å) using a linear 1% min$^{-1}$ acetoni-trile gradient (0–50% solvent B). The eluent was observed by dual wavelength UV detector set to 214 and 280 nm.

Author contributions—A. L. and N. L. D. designed the study and, along with C. C. C., wrote the paper. C. C. C., P. S. B., D. W., and L. D. synthesized and purified the peptides. D. W. carried out the mass spectrometry analyses. C. C. C. and N. L. D. determined the structure of the cyclic peptide. C. C. C., S. N., and P. G. carried out the animal experiments. All authors analyzed the results and approved the final version of the manuscript.

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