Network Fingerprint of Stimulation-Induced Speech Impairment in Essential Tremor

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Objective: This study was undertaken to gain insights into structural networks associated with stimulation-induced dysarthria (SID) and to predict stimulation-induced worsening of intelligibility in essential tremor patients with bilateral thalamic deep brain stimulation (DBS).

Methods: Monopolar reviews were conducted in 14 essential tremor patients. Testing included determination of SID thresholds, intelligibility ratings, and a fast syllable repetition task. Volumes of tissue activated (VTAs) were calculated to identify discriminative fibers for stimulation-induced worsening of intelligibility in a structural connectome. The resulting fiber-based atlas structure was then validated in a leave-one-out design.

Results: Fibers determined as discriminative for stimulation-induced worsening of intelligibility were mainly connected to the ipsilateral precentral gyrus as well as to both cerebellar hemispheres and the ipsilateral brain stem. In the thalamic area, they ran laterally to the thalamus and posteromedially to the subthalamic nucleus, in close proximity, mainly anterolaterally, to fibers beneficial for tremor control as published by Al-Fatly et al in 2019. The overlap of the respective clinical stimulation setting’s VTAs with these fibers explained 62.4% (p < 0.001) of the variance of stimulation-induced change in intelligibility in a leave-one-out analysis.

Interpretation: This study demonstrates that SID in essential tremor patients is associated with both motor cortex and cerebellar connectivity. Furthermore, the identified fiber-based atlas structure might contribute to future postoperative programming strategies to achieve optimal tremor control without speech impairment in essential tremor patients with thalamic DBS.

Essential tremor is the most common adult movement disorder, with an estimated prevalence of nearly 5% in populations >65 years old. For medication-refractory cases, deep brain stimulation (DBS) of the ventral intermediate nucleus of the thalamus (VIM) and the posterior subthalamic area (PSA) is an established, effective, and safe treatment.1,2 However, side effects such as stimulation-induced dysarthria (SID), ataxia, and muscle contractions may occur.3 Among these, SID is one of the most common and disabling side effects, affecting up to 75% of patients, interfering with quality of life and social functioning.4 Unfortunately, SID also impacts tremor control,
as it often leads to suboptimal stimulation settings to avoid speech problems.

The so far hypothesized pathogenesis of SID is a modulation of cerebellothalamic fibers and connections from the motor cortex (ie, the internal capsule), leading to a functional impairment of the speech motor system and hence a deterioration of speech intelligibility. Although these studies examined patients with Parkinson disease, previous studies by our group also showed an impairment of the speech motor system in essential tremor patients with thalamic DBS. Thalamic DBS led to an impairment of articulatory coordination patterns, probably due to a modulation of cerebellothalamic connections. Moreover, we observed articulatory imprecision and slowness affecting the production of the entire syllable cycle, most likely related to a modulation of the internal capsule. However, the exact pathogenesis of SID remains elusive.

Besides exploring the origin of SID, there is an urgent need to establish strategies to avoid SID while maintaining effective tremor control. Previous studies focused on the influence of lead placement and stimulation settings, and included dysarthria as a dichotomized symptom. In the present study, we chose speech intelligibility as the primary outcome parameter to predict the deterioration of speech under DBS. This measurement reflects real-life speech impairment and has been elaborated as a valid parameter for stimulation-induced impairment of the speech motor system. By combining measurements of speech intelligibility with a state-of-the-art normative structural connectome approach, we aimed to identify fibers predicting stimulation-induced worsening of intelligibility. In addition to offering insights into the networks associated with SID, these fibers might then serve as supportive atlas structures in postoperative programming sessions to avoid the occurrence of SID while maintaining effective tremor control.

Patients and Methods

Patient Selection and Ethics

Inclusion criteria were a confirmed diagnosis of medically intractable essential tremor according to the International Parkinson and Movement Disorder Society consensus diagnostic criteria, bilateral thalamic DBS implantation (VIM or VIM/PSA) at least 3 months before study participation, age > 18 and < 80 years, and German as native language. The occurrence of postoperative SID was not an inclusion criterion, and patients were not tested for voice tremor under inactivated stimulation before study participation. The study was carried out following the Declaration of Helsinki and was approved by the local ethics committee (17–425). All patients gave written informed consent before study participation.

Clinical Assessment

First, patients were assessed in “ON stimulation” state, with their regular stimulation settings as optimized per clinical routine, and in the “OFF stimulation” state after turning the stimulation off for at least 15 minutes. Second, a hemispherewise monopolar review was conducted with stimulation of the contralateral hemisphere turned off. When leads with 8 contact heights had been implanted (Vercise leads, Boston Scientific, Marlborough, MA), only every second contact, beginning at the tip, was included in the testing to increase spatial distribution and to diminish the examination time needed. All other leads (Cartesia leads, Boston Scientific; 3387/3389 leads, Medtronic, Dublin, Ireland) were tested at each of the 4 contact heights, with circular stimulation mode for directional contacts. Contacts were tested in randomized order to maintain blinding of the examiner and the patient to the order of the tested contacts. The frequency was set to 130Hz, and a pulse width of 60 microseconds was chosen for every patient. Before testing, impedances were measured to ensure the integrity of the DBS system and constant current mode was set if applicable.

Monopolar reviews were performed by increasing the stimulation amplitude in steps of 0.5mA until (1) a maximum of 10mA, (2) the occurrence of intolerable side effects, or (3) the onset of SID. The onset of SID was determined by a trained examiner (J.N.P.-S.), asking the patient to enumerate the names of the months repeatedly at each amplitude step. Furthermore, contralateral muscle contractions and ataxia, defined as contralateral dysmetria during the finger-to-nose test, were documented.

The following clinical assessments were conducted in (1) the “ON stimulation” state, (2) the “OFF stimulation” state, and (3) at each contact’s maximum stimulation amplitude as defined during the monopolar review.

Tremor Assessment. In the “ON stimulation” and “OFF stimulation” state, tremor severity was measured based on the Tremor Rating Scale (TRS). To shorten the duration of testing, tremor severity during the monopolar review was determined by the rater as postural tremor control of the contralateral arm, rated on a visual analogue scale (VAS) ranging from 0cm (“no tremor”) to 10cm (“most severe tremor”).

Speech Assessment. In each condition, patients were asked to enumerate the months and rate their “ability to speak” on a VAS ranging from 0cm (“normal”) to 10cm (“worst”). The examiner was kept blinded to the patient’s
Intelligibility Ratings and DDK Analysis. To investigate speech intelligibility perceived by naive listeners (all German native speakers), we extracted the sentence with the fewest reading errors from the natural sentence production task as auditory stimuli. We chose the sentence with the highest reading fluency to avoid effects of speech errors on the segmental and prosodic level on the intelligibility ratings and to increase the comparability of test sentences between the different stimulation settings. For natural sentence production, patients were instructed to read a short passage, a German standard text (“Nordwind und Sonne”/“Northwind and Sun”) at a comfortable speech rate.  

Intelligibility ratings and DDK Analysis. To investigate speech intelligibility perceived by naive listeners (all German native speakers), we extracted the sentence with the fewest reading errors from the natural sentence production task as auditory stimuli. We chose the sentence with the highest reading fluency to avoid effects of speech errors on the segmental and prosodic level on the intelligibility ratings and to increase the comparability of test sentences between the different stimulation settings. These were normalized to the same overall intensity level to minimize an effect of stimulus loudness on perception results. Eleven naive listeners rated the stimuli in a randomized order across the conditions but matched for patients to ensure blinding of the listeners to the stimulation condition. Each stimulus was evaluated on a VAS reaching from 1 point (“very bad intelligibility”) to 101 points (“very good intelligibility”). For further analysis, intelligibility rating per stimulus was calculated as the mean of all ratings across listeners.

The DDK labeling was carried out in a blinded manner by an experienced phonetician (T.T.), as described previously. In brief, syllable durations for each /kakaka/ sequence were identified from the start of the consonantal closure to the end of the vocalic opening with respect to the energy in the higher formant structure in the acoustic waveform. We used syllable duration as the most robust acoustic parameter described in the literature when objectively capturing the degree of motor speech impairment in DDKs. Prolonged syllable durations reflect an overall slowing down of the speech motor system and can be directly related to motor speech impairment. There is a debate in the literature on whether DDKs are comparable to natural sentence production. However, in a study on effects of thalamic DBS on speech production in essential tremor patients, Hermes et al have shown that slowing down of the speech motor system can be attested for both DDK tasks and natural sentence production. Furthermore, syllable duration has previously been shown to have a significant effect on intelligibility ratings and to be worsened by thalamic DBS in essential tremor patients.

Localisation of DBS Leads and Volume of Tissue Activated Estimation

DBS leads were localized with the Lead-DBS toolbox (www.lead-dbs.org). The detailed processing pipeline has been described elsewhere. In brief, postoperative computed tomographic (CT) images (IQon Spectral CT, iCT 256, Brilliance 256, Philips Healthcare, Best, the Netherlands) were linearly coregistered to preoperative magnetic resonance imaging (3T Ingenia, Achieva, 1.5T Ingenia, Philips Healthcare) using advanced normalization tools (ANTs, http://stnava.github.io/ANTS/, n = 13) or BRAINSFIT (https://github.com/BRAINSia/BRAINS Tools, n = 1) if ANTs did not provide sufficient results after visual inspection. Then images were nonlinearly normalized into standard space (ICBM 2009b NLIN asymmetric) using ANTs and the “effective (low variance)” strategy. DBS leads were automatically prereconstruced with the PaCER algorithm, manually refined, and corrected for postoperative brain shift as implemented in Lead-DBS. The orientation of directional leads was determined by the DiODE algorithm.

For each stimulation setting, volumes of tissue activated (VTA) were calculated in the patient’s native space and then transformed into standard space based on the individual nonlinear normalization. A well-established finite element method, introduced by Horn et al, was employed to estimate the spread of the electric field for homogenous tissue with a conductivity of \( \sigma = 0.15 \text{S/m} \). The VTA was thresholded at the electrical field isolevel of 0.19V/mm to reflect the clinical stimulation results of Mädlér and Coenen, adapted depending on the respective pulse width. Finally, right-sided VTAs were nonlinearly flipped to the left hemisphere using Lead-DBS for further analysis.
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Validation of Discriminative Fibers

Discriminative fibers were validated in a leave-one-out design.\textsuperscript{21,31,32} Briefly, discriminative fibers were recalculated for each patient based on the clinical assessments of all other patients. Then the respective number of discriminative fibers stimulated in the left-out patient’s “ON stimulation” state was summed up to conduct a linear regression analysis. This was done to investigate the influence of the amount of discriminative fibers stimulated on the percentage change of intelligibility in the “ON stimulation” state. An additional linear regression analysis was conducted to investigate the influence of the amount of fibers associated with tremor control, as identified by Al-Fatly et al\textsuperscript{31} on postoperative tremor control and stimulation-induced changes in intelligibility in “ON stimulation” setting.

Results

Patient Characteristics

Fourteen patients diagnosed with essential tremor (4 female) aged 65.4 (±13) years were prospectively recruited, resulting in 28 leads and 112 contacts investigated. Lead types and clinical stimulation settings are described in the Table 1. All patients were right-handed and bilaterally implanted either targeting the VIM (n = 2) or the VIM/PSA (n = 12) with a mean time of 29.2 (±24) months since implantation.

Comparison of “OFF Stimulation” and “ON Stimulation” State

The mean rating of intelligibility did not differ significantly between “OFF stimulation” and “ON stimulation” state on the group level (mean OFF: 70.9 ± 14.3, mean ON: 67.5 ± 17.1, \( p = 0.763\); Fig 1A1). However, on the individual level, a formal worsening of intelligibility rating was observed in one-half of the patients. Regarding impairment of the speech motor system, syllable durations increased significantly during “ON stimulation” (mean OFF: 243 ± 58 milliseconds, mean ON: 275 ± 72 milliseconds, \( p = 0.011\); see Fig 1B1). Regarding tremor control, TRS total scores improved significantly with clinical stimulation settings (mean OFF: 35.2 ± 18.4, mean ON: 13.0 ± 10.4, \( p < 0.001\); see Fig 1C1), reflecting a tremor suppression of >60%.

Monopolar Review Outcomes

Figure 2 illustrates the anatomical position of investigated contacts and the stimulated region covering the VIM and the PSA. A total of 111 stimulation settings were included for further analysis (Fig 3). When comparing the “OFF stimulation” state to stimulation settings not causing SID and stimulation settings causing SID, Kruskal–Wallis test revealed differences in intelligibility ratings (\( \chi^2 \[2\] = 14.1, p < 0.001\); see Fig 1A2). Post hoc Wilcoxon rank sum tests showed significant differences in “OFF” versus “SID” (mean “SID”: 58.2 ± 15.6, \( p = 0.007\)) and “no SID” versus “SID” (mean “no SID”: 68.5 ± 14.7, \( p < 0.001\)). Additionally, for syllable durations, Kruskal–Wallis test (\( \chi^2 \[2\] = 15.6, p < 0.001\)) and post hoc Wilcoxon rank sum tests also revealed significant differences for “OFF” versus “SID” (mean “SID”: 293 ± 72 milliseconds, \( p = 0.011\)) and “no SID” versus “SID” (mean “no SID”: 247 ± 51 milliseconds, \( p < 0.001\)). When assessing the ability to speak, using the VAS, there was a worsening from “no SID” to “SID” (mean “no SID”: 2.0 ± 2.0, mean “SID”: 3.9 ± 2.0, \( p < 0.001\)).

structural connectome.\textsuperscript{33} This structural connectome has previously been used to successfully predict tremor outcomes after thalamic DBS in essential tremor patients\textsuperscript{31} and is based on diffusion data collected in 20 subjects using a single-shot spin-echo planar imaging sequence (repetition time = 10,000 milliseconds, echo time = 94 ms, 2 x 2 x 2 mm\textsuperscript{3}, 69 slices). Global fiber-tracking was performed using Gibb’s tracking method,\textsuperscript{34} and the resulting fibers were warped into standard space.\textsuperscript{33} In the present study, each of these fibers’ discriminative value was tested by associating the fiber’s connectivity to VTAs across patients with the respective change in intelligibility. Specifically, a linear mixed effect model was set up for each fiber connected to at least 20 VTAs, to test for differences between changes in speech intelligibility of connected and unconnected VTAs. The grouping variable (unconnected/connected) was included as a fixed effect and to reflect that 2 leads per patient and a total of 28 leads were tested; the respective lead and patient were included as random effects, with lead treated as nested effect within each patient. Change scores were calculated as percentage change from “OFF stimulation” state ([intelligibility \textunderscore endpoint − intelligibility \textunderscore OFF stimulation]/intelligibility \textunderscore OFF stimulation) and divided by the respective amplitude as proposed by Dembek et al\textsuperscript{30} as changes in intelligibility in “ON stimulation state” were highly correlated with stimulation amplitude (rho = −0.66, \( p = 0.01\)). When connected VTAs led to worsening of speech intelligibility in comparison to unconnected VTAs with a \( p \) value < 0.05, a fiber was determined as discriminative. Importantly, “ON stimulation” state VTAs were not included in the determination of discriminative fibers.
When assessing postural tremor control, using the VAS, data suggested significant improvement from “OFF” to “no SID” and “OFF” to “SID” (mean “OFF”: 5.9 ± 1.6, mean “no SID”: 1.0 ± 1.3, \( p < 0.001 \); mean “SID”: 1.0 ± 1.1, \( p < 0.001 \)). Intelligibility ratings significantly correlated to the patients’ VAS rating of their ability to speak (rho = −0.45, \( p < 0.001 \)) and syllable durations (rho = −0.66, \( p < 0.001 \)). As shown in Figure 3, onset of SID was associated with muscle contractions and/or ataxia, but also occurred without any additional symptoms.

### Discriminative Fibers for Worsening of Intelligibility

Fibers determined as discriminative for stimulation-induced worsening of intelligibility were mainly connected to the ipsilateral precentral gyrus as well as to both cerebellar hemispheres and the ipsilateral brain stem (Fig 4). In the target area, they ran laterally to the thalamus and posteromedially to the subthalamic nucleus (STN), in close proximity, mainly anterolaterally, to fibers beneficial for tremor control as published by Al-Fatly et al. \(^3^1\) Some of them even overlapped (Fig 5). Validation of the

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**TABLE 1. Clinical Stimulation Settings**

| Patient | Lead Type     | Clinical Stimulation Settings | Left Hemisphere | Right Hemisphere |
|---------|---------------|-------------------------------|-----------------|------------------|
| 1       | Cartesia, Boston Scientific | C+; 2−, 21%; 3−, 5%; 4−, 29%; 5−, 17%; 6−, 5%; 7−, 23%; 60μs; 149Hz; 2.3mA | C+; 10−, 17%; 11−, 26%; 12−, 27%; 13−, 10%; 14−, 10%; 15−, 10%; 60μs; 149Hz; 2.3mA |
| 2       | Cartesia, Boston Scientific | C+; 5+, 34%; 6+, 33%; 7+, 33%; 1−, 90%; 2−, 5%; 4−, 5%; 40μs; 204Hz; 5.0mA | C+; 13+, 34%; 14+, 33%; 15+, 33%; 9−, 80%; 11−, 10%; 12−, 10%; 40μs; 204Hz; 4.7mA |
| 3       | 3387, Medtronic | C+; 1−, 100%; 60μs; 180Hz; 3.0mA | C+; 9−, 100%; 60μs; 180Hz; 1.9mA |
| 4       | Cartesia, Boston Scientific | C+; 2−, 100%; 60μs; 130Hz; 3.6mA | C+; 10−, 29%; 11−, 43%; 12−, 28%; 60μs; 130Hz; 1.9mA |
| 5       | Cartesia, Boston Scientific | C+; 2−, 34%; 3−, 33%; 4−, 33%; 60μs; 130Hz; 2.1mA | C+; 10−, 34%; 11−, 33%; 12−, 33%; 60μs; 130Hz; 2.1mA |
| 6       | Vercise, Boston Scientific | C+; 3−, 100%; 60μs; 130Hz; 3.2mA | C+; 11−, 100%; 60μs; 174Hz; 2.3mA |
| 7       | 3389, Medtronic | C+; 2−, 100%; 60μs; 130Hz; 3.7mA | C+; 10−, 100%; 60μs; 130Hz; 2.0mA |
| 8       | Vercise, Boston Scientific | C+; 3−, 100%; 60μs; 174Hz; 1.3mA | C+; 11−, 100%; 60μs; 174Hz; 0.7mA |
| 9       | Vercise, Boston Scientific | C+; 3−, 100%; 60μs; 130Hz; 3.8mA | C+; 11−, 100%; 60μs; 130Hz; 2.9mA |
| 10      | 3389, Medtronic | Vim 1: C+; 0−; 2.0V; 60μs; 125Hz; Vim 2: C+; 1−; 2.5V; 60μs; 125Hz | Vim 1: C+; 8−; 2.0V; 60μs; 125Hz; Vim 2: C+; 9−; 2.7V; 60μs; 125Hz |
| 11      | Vercise, Boston Scientific | C+; 5+, 100%; 2−, 70%; 3−, 30%; 60μs; 174Hz; 2.1mA | C+; 13+, 100%; 10−, 70%; 11−, 30%; 60μs; 174Hz; 2.1mA |
| 12      | Cartesia, Boston Scientific | C+; 1−, 100%; 50μs; 185Hz; 1.4mA | C+; 13−, 35%; 14−, 35%; 15−, 30%; 60μs; 185Hz; 1.2mA |
| 13      | Cartesia, Boston Scientific | C+; 2−, 34%; 3−, 33%; 4−, 33%; 60μs; 185Hz; 1.2mA | C+; 10−, 34%; 11−, 33%; 12−, 33%; 60μs; 185Hz; 1.6mA |
| 14      | Cartesia, Boston Scientific | C+; 1−, 100%; 60μs; 130Hz; 1.2mA | C+; 9−, 100%; 60μs; 130Hz; 1.2mA |
discriminative fibers in a leave-one-out design revealed that the overlap of the VTAs with the discriminative fibers identified in the present study could explain 62.4% of the variance in individual intelligibility outcome with clinical stimulation settings as measured in the respective “ON stimulation” state ($R^2 = 0.624$, $p < 0.001$; see Fig 4). Overlap of the VTAs with these discriminative “speech” fibers was not associated with postoperative tremor control.
(R^2 = 0.04, p = 0.289), and overlap of these VTAs with fibers associated with tremor control, as published by Al-Fatly et al., was associated with neither postoperative tremor control (R^2 = 0.02, p = 0.524) nor stimulation-induced changes in intelligibility in our cohort (R^2 = 0.003, p = 0.856).

**Discussion**

This study demonstrates that stimulation-induced speech impairment in thalamic DBS for essential tremor patients is associated with both motor cortex and cerebellar connectivity. Furthermore, the identified discriminative fibers were predictive for worsening of intelligibility with clinical stimulation settings in our cohort.

**Discriminative Fibers to Predict Worsening of Intelligibility**

Discriminative fibers for stimulation-induced worsening of intelligibility were identified to run laterally to the motor thalamus and posteromedially to the STN. These fibers were either nearby, mainly anterolaterally, or even overlapping with fibers beneficial for tremor control as published by Al-Fatly et al. The overlap of the clinical stimulation settings with these fibers was predictive of 62.4% of the variance of stimulation-induced changes of intelligibility.
Intelligibility, as revealed in a leave-one-out design (see Figs 4 and 5). It remains unclear whether the fibers for speech impairment and tremor improvement are distinct, as we were unable to identify fibers for tremor control in this cohort due to the study design. Therefore, we employed the fibers as identified by Al-Fatly et al in the same connectome. In our analysis, overlap with these “tremor” fibers was predictive neither for postoperative tremor control nor for stimulation-induced changes in intelligibility. Furthermore, one has to bear in mind that these fibers were designed to illustrate predictive cortical connectivity profiles on a structural level and not as an individual predictor of postoperative tremor control.

Intelligibility was chosen as a parameter representing the degree of SID in essential tremor patients because it indicates a deterioration of the speech motor system and represents the patient-rated “ability to speak,” and is therefore of high clinical relevance in daily living. In contrast to previous studies, no worsening of intelligibility rating was observed with bilateral DBS on the group level when comparing “ON stimulation” and “OFF stimulation.” This finding might be due to some patients in the present cohort having a voice tremor during “OFF stimulation,” which has been reported to improve with DBS, and thereby might have led to an improvement of intelligibility beyond its worsening due to an affection of the glottal speech motor system (see Fig 1). Nevertheless, on the individual level, 50% of the patients experienced a worsening of intelligibility with clinical stimulation settings, and there was a significant increase in syllable duration under DBS, indicating a systematic affection of the speech motor system in terms of oral control in our cohort. Of note, the identified fibers seem to be specific for changes in intelligibility, as they were not predictive for tremor control.

**Pathophysiological Considerations**

Following Fuertinger et al and Guenther and Vladusich, the functional connectome of real-life speech production in right-handed healthy subjects is constituted by a core hub network, centered on the left laryngeal and orofacial regions of the primary motor cortex and its main input regions in the surrounding premotor, somatosensory, and parietal cortices. This core sensorimotor hub network is then widely connected to other brain regions, such as the auditory cortex as an auditory feedback control subsystem, the parietal cortex for phonological and semantic processing, or the cerebellum for modulation of vocal motor timing and sequence processing.

As expected and hypothesized in previous studies and in line with the described connectome of real-life speech production, the identified discriminative fibers mainly connected the motor cortex to the brain stem and both cerebellar hemispheres. The association

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**FIGURE 3:** Clinical symptoms associated with stimulation-induced dysarthria (SID). Clinical symptoms of motor cortex (muscle contractions) or cerebellar cortex (ataxia) involvement at the onset of SID are shown. One contact was excluded because the patient experienced side effects severely interfering with further testing.
between stimulation-induced speech impairment and these cortical areas is underlined by the finding that the onset of SID was in most of the cases associated with clinical symptoms of motor cortex modulation (ie, muscle contractions) or cerebellar cortex involvement (ie, ataxia; see Fig 3). The course of these fibers also fits the finding of previous studies reporting that a more lateral contact position and contacts located outside the motor thalamus might be associated with SID in essential tremor patients. Additionally, damage to the cerebellum, especially the paravermal region, has previously been reported to result in slurred and poorly coordinated speech, as also observed in essential tremor patients with DBS. Although indicating stimulation-induced speech impairment by cerebellar involvement, the present finding cannot be predictive of later cerebellar syndrome induction, as discussed in essential tremor patients with thalamic DBS. Previous studies investigating changes in intelligibility after DBS of the STN in Parkinson disease provided evidence that both modulation of motor fibers running in the internal capsule and a modulation of cerebellothalamic pathways (ie, the dentatorubrothalamic tract) can induce stimulation-induced speech worsening. Interestingly, the course of the discriminative fibers is in line with a study by Aström et al reporting a posteromedial contact position in relation to the STN to be associated with impairment of speech intelligibility in patients with Parkinson disease treated with DBS of the STN. Especially in the PSA, the identified discriminative fibers were running quite strictly separated, anterior and lateral to the fibers associated with tremor control (see Fig 5). However, this study does not provide specific connectivity patterns.
to the cerebellar cortex or the motor cortex differentiating between fibers associated with tremor control and fibers predicting stimulation-induced speech impairment. Taking together the results of the present study and of previous studies provides evidence for a combination of spastic and atactic changes in the speech motor system,\textsuperscript{8,9} and this pathophysiological correlate seems to hold true for SID in patients with essential tremor.

**Methodological Considerations and Limitations**

Whereas previous studies focused on phonematic and articulographic features of SID,\textsuperscript{8,9,11,13} this study expands these findings by (1) revealing the structural network underlying SID and (2) providing an atlas structure predictive of stimulation-induced changes in intelligibility. Furthermore, this study highlights the spatial proximity of tremor control and SID, which is often experienced in clinical practice and may lead to suboptimal postoperative tremor control. Although the cohort-size of 14 patients might seem small, a total of 111 stimulation settings could be included in the analysis. To estimate the VTAs based on these stimulation settings, a well-established approach was used that has previously been employed to identify optimal target regions and connectivity profiles in Parkinson disease and essential tremor.\textsuperscript{21,24,30,31,42} However, the theoretical concept of VTA modeling constitutes a simplification that neglects factors like fiber orientation.\textsuperscript{43} Regarding the concept of predicting effects of DBS in relation to the anatomical target area, there have been several approaches in the past, such as investigating lead positions,\textsuperscript{1} the creation of probabilistic sweet spots,\textsuperscript{30,42} and the estimation of beneficial connectivity profiles.\textsuperscript{21,31}

In this study, we focused on providing an atlas structure that is easy to implement in planning and programming software and therefore decided to base our predictive model on a well-established approach introduced by

\textbf{FIGURE 5: Comparison of discriminative fibers for changes of intelligibility and tremor control. (A)} The course of discriminative fibers for changes of intelligibility (pink) and postoperative tremor control (green), as identified by Al-Fatly et al.,\textsuperscript{31} in lateral (A1) and posterior view (A2), together with the thalamus (yellow), the ventral intermediate nucleus (VIM; blue), and the subthalamic nucleus (STN; light gray). (B) Course of the respective fibers in axial view with overlapping areas marked in orange. Slice positions are indicated in A1. For increased clarity, only voxels with at least 6 neighboring voxels containing the respective fiber tracts are shown. Anatomical structures are taken from the DISTAL atlas, as included in Lead-DBS.\textsuperscript{20,35} A = anterior; L = lateral; M = medial; P = posterior; RN = red nucleus; Th = thalamus.
Baldermann et al. In these studies including clinical stimulation settings only, $t$ tests and $T$ statistics were employed to define discriminative fibers and to predict the respective outcome parameter. In contrast, in the present study, determination of discriminative fibers was based on linear mixed effect models to control for multiple testing per patient. Some methodological limitations should be considered when interpreting the results of this study. First, the sample size of the present study is limited to 14 patients, which is within the range of previous studies examining deterioration of the speech motor system in essential tremor patients with thalamic DBS. In contrast to these studies mainly comparing “OFF stimulation” state to “ON stimulation” state, the present study included 10 test settings per patient. However, the limited sample size is not fully overcome by the larger number of stimulation settings. Nevertheless, and despite the reduced spread of patients with varying severities of SID, the results held true in the leave-one-out analysis. Second, VTAs were pooled on the left hemisphere for the analysis. This approach seems appropriate, as all patients were right-handed and previous studies did not show any difference between right and left hemispheric DBS regarding SID in bilaterally implanted essential tremor patients. However, there are studies reporting SID to be associated with left-hemispheric stimulation of the STN in Parkinson disease. Third, an atlas-based approach neglects a certain degree of interindividual heterogeneity, but the employed state-of-the-art multispectral coregistration approach has proved to be accurate. Fourth, this study employed normative connectome data to estimate structural connectivity in individual patients. This approach has already been implemented in many studies investigating the effects of DBS when patient-specific imaging data allowing fiber tracking was lacking, for example, in Parkinson disease and obsessive–compulsive disorder, but also essential tremor. Although these connectomes do not represent patient-specific connectivity, they are superior in quality to most images acquired during clinical routine by using specialized magnetic resonance hardware and best-performing tractography processing algorithms. Most importantly, using this specific normative connectome data allowed us to compare our results regarding SID to the results by Al-Fatly et al regarding tremor suppression without being biased by different imaging acquisition protocols. Lastly, interindividual anatomical variability and center-specific targeting strategies might lead to different target points. This raises the question of the generalizability of our results to other cohorts. Therefore, future studies, including different centers and target points, are warranted to create more generally applicable predictive models.

Conclusion
The present study demonstrates that connectivity to both the motor cortex and the cerebellum is associated with stimulation-induced speech impairment in essential tremor patients. Furthermore, the derived fiber-based atlas structure might help to avoid SID in essential tremor patients and could easily be implemented in postoperative programming strategies.

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Author Contributions
J.N.P.-S., H.J., T.T., T.A.D., and M.T.B. contributed to the conception and design of the study; all authors contributed to the acquisition and analysis of the data; J.N.P.-S., H.J., and T.A.D., contributed to drafting the text and preparing the figures.

Potential Conflicts of Interest
J.N.P.-S., J.K.S., P.R., V.V.-V., T.A.D., and M.T.B. have business relations with at least one of Medtronic, Abbott, and Boston Scientific, which produce DBS devices, but none is related to the current work.

References
1. Barbe MT, Reker P, Hamacher S, et al. DBS of the PSA and the VIM in essential tremor: a randomized, double-blind, crossover trial. Neurology 2018;91:e543–e550.
2. Schuurman PR, Bosch DA, Bossuyt PM, et al. A comparison of continuous thalamic stimulation and thalamotomy for suppression of severe tremor. N Engl J Med 2000;342:461–468.
3. Fytagoridis A, Astrom M, Wardell K, Blomstedt P. Stimulation-induced side effects in the posterior subthalamic area: distribution, characteristics and visualization. Clin Neurol Neurosurg 2013;115:65–71.
4. Palma R, Lyons KE, Wilkinson SB, et al. Long-term evaluation of deep brain stimulation of the thalamus. J Neurosurg 2006;104:506–512.
5. Aström M, Tripoliti E, Hariz MI, et al. Patient-specific model-based investigation of speech intelligibility and movement during deep brain stimulation. Stereotact Funct Neurosurg 2010;88:224–233.
6. Fenoy AJ, McHenry MA, Schiess MC. Speech changes induced by deep brain stimulation of the subthalamic nucleus in Parkinson disease: involvement of the dentatorubrothalamic tract. J Neurosurg 2017;126:2017–2027.
7. Mahlknecht P, Akram H, Georgiev D, et al. Pyramidal tract activation due to subthalamic deep brain stimulation in Parkinson’s disease. Mov Disord 2017;32:1174–1182.

8. Mücke D, Hermes A, Roetter TB, et al. The effects of thalamic deep brain stimulation on speech dynamics in patients with essential tremor: an articulography study. PLoS One 2018;13:e0191359.

9. Mücke D, Becker J, Barbe MT, et al. The effect of deep brain stimulation on the speech motor system. J Speech Lang Hear Res 2014; 57:1206–1218.

10. Hermes A, Mücke D, Thies T, Barbe MT. Coordination patterns in essential tremor patients with deep brain stimulation: syllables with low and high complexity. Lab Phonol 2019;10.6.

11. Becker J, Barbe MT, Hartinger M, et al. The effect of uni- and bilateral thalamic deep brain stimulation on speech in patients with essential tremor: acoustics and intelligibility. Neuro modulation 2017; 20:223–232.

12. Matsumoto JY, Fossett T, Kim M, et al. Precise stimulation location optimizes speech outcomes in essential tremor. Parkinsonism Relat Disord 2016;32:60–65.

13. Becker J, Thies T, Petry-Schmelzer JN, et al. The effects of thalamic and posterior subthalamic deep brain stimulation on speech in patients with essential tremor—a prospective, randomized, double-blind crossover study. Brain Lang 2020;202:104724.

14. Moyer SB. Repeated reading. J Learn Disabil 1982;15:619–623.

15. Caspers J. The influence of erroneous stress position and segmental errors on intelligibility, comprehensibility and foreign accent in Dutch as a second language. Linguistics Netherlands 2010;27:17–29.

16. Therrien WJ. Fluency and comprehension gains as a result of repeated reading: a meta-analysis. Remedial Spec Educ 2004;25:252–261.

17. Ackermann H, Hertrich I, Hehr T. Oral diadochokinesis in neurologi-cal dystonias. Folia Phoniati Logop 1995;47:15–23.

18. Staiger A, Schölderle T, Brendel B, et al. Oral motor abilities are task dependent: a factor analytic approach to performance rate. J Mot Behav 2017;49:482–493.

19. Hermes A, Mücke D, Thies T, Barbe MT. Intragestural variation in natural sentence production: essential tremor patients treated with DBS. Proc Interspeech 2019;2019:4539–4543.

20. Horn A, Li N, Dembek TA, et al. Lead-DBS v2: towards a comprehensive pipeline for deep brain stimulation imaging. Neuroimage 2019;184:293–316.

21. Horn A, Reich M, Vorwerk J, et al. Connectivity predicts deep brain stimulation outcome in Parkinson’s disease. Ann Neurol 2017;82:67–78.

22. Klein A, Andersson J, Ardekani BA, et al. Evaluation of 14 nonlinear deformation algorithms applied to human brain MRI registration. Neuroimage 2009;46:786–802.

23. Johnson H, Harris G, Williams K. BRAINSFit: mutual information registrations of whole-brain 3D images, using the insight toolkit. Insight J 2007;57.2.

24. Petry-Schmelzer JN, Krause M, Dembek TA, et al. Non-motor outcomes depend on location of neurostimulation in Parkinson’s disease. Brain 2019;142:3592–3604.

25. Ewert S, Horn A, Finkel F, et al. Optimization and comparative evaluation of nonlinear deformation algorithms for atlas-based segmentation of DBS target nuclei. Neuroimage 2019;184:536–598.

26. Husch A, Petersen MV, Gemmar P, et al. PaCER—a fully automated method for electrode trajectory and contact reconstruction in deep brain stimulation. Neuroimage Clin 2018;17:80–89.

27. Dembek TA, Hoevels M, Hellerbach A, et al. Directional DBS leads show large deviations from their intended implantation orientation. Parkinsonism Relat Disord 2019;67:117–121.

28. Astrom M, Diczfalusy E, Martens H, Wardell K. Relationship between neural activation and electric field distribution during deep brain stimulation. IEEE Trans Biomed Eng 2015;62:664–672.

29. Maderl B, Coenen VA. Explaining clinical effects of deep brain stimulation through simplified target-specific modeling of the volume of activated tissue. AJNR Am J Neuroradiol 2012;33:1072–1080.

30. Dembek TA, Barbe MT, Astrom M, et al. Probabilistic mapping of deep brain stimulation effects in essential tremor. Neuroimage Clin 2017;13:164–173.

31. Al-Faty B, Ewert S, Kübler D, et al. Connectivity profile of thalamic deep brain stimulation to effectively treat essential tremor. Brain 2019;142:3086–3098.

32. Baldermann JC, Melzer C, Zapf A, et al. Connectivity profile predictive of effective deep brain stimulation in obsessive-compulsive disorder. Biol Psychiatry 2019;85:735–743.

33. Horn A. A structural group-connectome in standard stereotactic (MNI) space. Data Brief 2015;5:292–296.

34. Reisert M, Mader I, Anastasopoulos C, et al. Global fiber reconstruction becomes practical. Neuroimage 2017;54:955–962.

35. Ewert S, Pleitig P, Li N, et al. Toward defining deep brain stimulation targets in MNI space: a subcortical atlas based on multimodal MRI, histology and structural connectivity. Neuroimage 2018;170:271–282.

36. Sandstrom L, Blomstedt P, Karlsson F. Voice tremor response to deep brain stimulation in relation to electrode location in the posterior subthalamic area. World Neurosurg X 2019;3:100024.

37. Fuertinger S, Horwitz B, Simonyan K. The functional connectome of speech control. PLoS Biol 2015;13:e1002209.

38. Guenther FH, Vlachutich T. A neural theory of speech acquisition and production. J Neurolinguistics 2012;25:408–422.

39. Ackermann H, Mathiak K, Recker A. The contribution of the cerebellum to speech production and speech perception: clinical and functional imaging data. Cerebellum 2007;6:202–213.

40. Ackermann H, Vogel M, Petersen D, Poremba M. Speech deficits in ischaemic cerebellar lesions. J Neurol 1992;239:223–227.

41. Reich MM, Brumberg J, Pozzi NG, et al. Progressive gait ataxia following deep brain stimulation for essential tremor: adverse effect or lack of efficacy? Brain 2016;139:2948–2956.

42. Dembek TA, Roediger J, Horn A, et al. Probabilistic sweet spots predict motor outcome for deep brain stimulation in Parkinson disease. Ann Neurol 2019;86:527–538.

43. Andersson DN, Duffley G, Vorwerk J, et al. Anodic stimulation misunderstood: preferential activation of fiber orientations with anodic waveforms in deep brain stimulation. J Neural Eng 2019;16:016026.

44. Irmen F, Horn A, Mosley P, et al. Left prefrontal impact links subthalamic stimulation with depressive symptoms. Ann Neurol 2020; 87:962–975.

45. Li N, Baldermann JC, Klimeur A, et al. A unified connectomic target for deep brain stimulation in obsessive-compulsive disorder. Nat Commun 2020;11:3364.

46. Tripoliti E, Zrinzo L, Martinez-Torres I, et al. Effects of subthalamic stimulation on speech of consecutive patients with Parkinson disease. J Neurolinguistics 2011;24:80–96.

47. Tripoliti E, Limousin P, Foltynie T, et al. Predictive factors of speech intelligibility following subthalamic nucleus stimulation in consecutive patients with Parkinson’s disease. Mov Disord 2014;29:532–538.

48. Groppa S, Herzog J, Falk D, et al. Physiological and anatomical decomposition of subthalamic neurostimulation effects in essential tremor. Brain 2014;137:109–121.

49. Fillard P, Descoteaux M, Goh A, et al. Quantitative evaluation of 10 tractography algorithms on a realistic diffusion MR phantom. Neuroimage 2011;56:220–234.