Transcutaneous multichannel electrogastrography: normal parameters in a Brazilian population

Nayara Salgado CARVALHO1,2, Diego Cardoso BAIMA1, Ricardo Correa BARBUTI1, Paulo Jose Pereira Campos CARVALHO2, Joffre REZENDE FILHO3 and Tomas NAVARRO-RODRIGUEZ1

ABSTRACT – Background – Electrogastrography (EGG) is a noninvasive technique for the assessment of gastric myoelectrical activity using electrodes placed on the abdominal surface. Changes in gastric myoelectrical activity may be associated with diseases such as gastroparesis, functional dyspepsia, nausea, and recurrent vomiting. In Brazil, no studies to date have assessed gastric myoelectrical activity using multichannel EGG in healthy individuals. Objective – To establish normal values of transcutaneous multichannel EGG in healthy Brazilian individuals. Methods – This was a prospective study including 20 healthy individuals who underwent EGG. Recording was performed during two periods: a preprandial recording was performed for 30 minutes, and a postprandial recording was performed for 30 minutes after a soft-solid meal of 400 kcal (20 grams of proteins, 60 grams of carbohydrates, and 9 grams of fat). Results – We assessed dominant frequency (DF) parameters, %DF distribution, the instability coefficient, and the power ratio (PR). A total of 20 individuals (11 women and 9 men) with a mean age of 39.5±7.4 years were included. Mean DF (%DF) ranged from 2.4 to 3.1 cpm in the resting phase and 2.6 to 3.2 cpm in the postprandial period. The %DF in normogastria range was >70% in all healthy individuals. We identified that only one individual did not present a positive response to the test meal, and the other 19 individuals showed a PR greater than 1. The instability coefficient did not change significantly with meal intake. Conclusion – Multichannel EGG may be applied in future studies to evaluate gastric motility disorders in the Brazilian population.

INTRODUCTION

Electrogastrography (EGG) is a noninvasive technique used to assess the myoelectrical activity of the stomach through electrodes placed on the abdominal surface. In 1922, Alvarez described the first EGG recordings, but it was only in the 1950s when Davis and Gershon began the first studies to systematize the technique. Since 1990, with the introduction of computerized signal analysis, EGG has been popularized. The gastric myoelectrical activity consists of slow waves (electrical control activity) and electrical potentials termed spikes (electrical response activity). Over time, studies have evaluated the simultaneous recordings of skin electrodes and serosal or mucosal electrodes, demonstrating that EGG captures the gastric myoelectrical activity. A recent study reviewed the validity of EGG, including the relationship between EGG and the internal serosal recording of slow waves of the stomach and between EGG and gastric contractions. Lin et al. (2000) correlated serosal recording with EGG in the evaluation of the postprandial response of gastric myoelectrical activity.

Recording of gastric myoelectrical activity with skin electrodes is subject to numerous movement artifacts and electrical interferences from other organs. The applicability and reproducibility of the method have depended on technological developments over time, the manner in which the examinations were recorded, appropriate equipment settings, development of new amplifiers and filters, and the use of multichannel equipment with bipolar electrodes that offer better signal quality.

Gastrointestinal motility disorders, functional gastrointestinal tract diseases, or inducing stimuli can alter the myoelectrical activity of the stomach, leading to EGG abnormalities. The normal slow wave frequency in humans is three cycles per minute (cm). Abnormalities in gastric myoelectrical activity include dysrhythmias that can be classified as bradygastria, tachygastria, and arrhythmia. Studies that evaluated the recording of gastric myoelectrical activity with serosal electrodes defined the following, according to frequency range: normogastria, two to four cm; bradygastria, 0.5 to two cm; and tachygastria, four to nine cm. However, the variation in the frequency of gastric myoelectrical activity considered normal has been reported with widely different values, such as two to four cm; two to 4.5 cm; two to 4.5 cm; two to 4.5 cm; and 2.4 to 3.7 cm. This frequency variation can alter the percentages of normogastria, bradygastria, and tachygastria in the EGG analysis; therefore, these values are important.

A review of Brazilian demographic data published by the Brazilian Institute of Geography and Statistics (Instituto Brasileiro de Geografia e Estatística - IBGE) in 2010 indicated that the ethnic and racial composition of the Brazilian population is the result of a confluence of people of various origins, with 33% of Amerindian origin, 28% of African origin, and 39% of European origin. This finding raised the question of whether the parameters of normal...
ity in the literature should be used in Brazil. In addition, studies conducted in Brazil were performed with single-channel EGG devices[26,31]. No multichannel EGG studies have been conducted in the Brazilian population; therefore, the aim of this study was to evaluate the gastric myoelectrical activity and to define parameters of normality for multichannel EGG in a Brazilian population.

METHODS

Subjects
The study protocol was approved by the Ethics Committee of Hospital das Clínicas de São Paulo, University of São Paulo (register number 16442). All participants signed a free and informed consent form. The EGG examination was performed at the Gastroenterology Diagnostics Center, Hospital das Clínicas, São Paulo. Healthy volunteers without dyspeptic symptoms were invited to participate in the study. Participants were aged between 18 and 70 years and had a body mass index (BMI) <30 kg/m². The exclusion criteria were any previously diagnosed condition, previous gastrointestinal tract surgery, psychiatric illness, any medication that could affect gastrointestinal function (e.g. prokinetics, antihypertensives, beta-blockers, antidepressants), pregnancy, lactation, and alcohol consumption. Data from 20 healthy volunteers (11 women and 9 men) with a mean age of 41±10 years were included in the final analysis.

Multichannel EGG
Multichannel EGG was performed with the Polygraf Solar EGG module electrogastrography system developed by Medical Measurement Systems – MMS (Laborie Europe, Enschede, The Netherlands), which is composed of six bipolar electrodes, one reference electrode, one ground electrode, and a strap for recording respiratory movement.

• Skin preparation
At the abdominal site where the electrodes were positioned, the skin was completely cleaned, and abrading with sandpaper was performed to ensure that the impedance between the electrode pairs remained low.

• Electrode placement
The MMS Ag/AgCl electrodes (N-00-S, MMS) were positioned in the abdominal region on top of the skin. The ground electrode was placed in an area with little movement and distant from the stomach (near the right shoulder), and the respiratory strap was placed in the lower thoracic region. The other six electrodes were arranged on the mesogastrium as follows: electrode three, used as the main electrode, was placed two cm above the midpoint between the xiphoid process and the navel; another two electrodes were placed 45° to the upper left side of the main electrode (electrodes one and two). Another electrode was placed four cm to the right and on the same line as main electrode three (electrode four). Two more electrodes were placed two cm below main electrode three on the left and right sides (electrodes five and six, respectively) [4,35,37,39].

• Subject position
The examination was performed with the volunteers in a comfortable supine position so that there was no or minimal body movement. EGG records were performed at the same time of day. The subject was instructed not to speak, move, read, or make phone calls during the procedure to ensure that the position was the same throughout the recording. Whenever inevitable body movement or artifacts occurred, the time was written down, and these segments were removed from the analysis. The volunteers were also instructed not to fall asleep during the recording [37].

• Recording duration
EGG was performed without recording for 10 to 15 minutes until the tracing was stabilized, and recordings were performed in two periods: the first 30-minute period was performed with the patient under fasting conditions for eight hours, and the second 30-minute period was performed after ingestion of the test meal [38]. The test meal consisted of 20 grams of protein, 60 grams of carbohydrates, and 9 grams of fat, totaling 400 kcal [39].

• EGG signal analysis
The recorded EGG signal was subjected to visual and computerized analysis. Visual analysis was performed to eliminate movement artifacts. Fast Fourier transform (FFT) and running spectral analysis were applied in the computerized analysis. The raw EGG signal recording and FFT power plot and running spectral analysis of the EGG signal are shown in Figure 1 [38]. Each running spectrum was four minutes and 16 seconds long. The frequencies of each spectrum were interpreted by FFT and were classified as follows: bradygastria (1–2 cpm), normogastria (2–4 cpm), tachygastria (4–10 cpm), and duodenal/respiratory rhythm (10–15 cpm) [35]. The following parameters, derived from the computerized EGG signal analysis, were determined [18,35,37,39]:
(i) mean dominant frequency (DF) at baseline and in the postprandial period and the dominant power (DP). The mean DF is the frequency with the highest mean potential in the spectrum. The frequency that occurs at the highest gastric potential is determined by the absolute peak value, and the mean frequency and power are calculated by averaging the individual spectra;
(ii) percentage of the DF in normogastria (2–4 cpm), bradygastria (1–2 cpm), tachygastria (4–10 cpm), and duodenal/respiratory origin (10–15 cpm). This evaluation was performed using the running spectral analysis method and by calculating the percentage distribution in these frequency ranges (normogastria, bradygastria, tachygastria, and duodenal/respiratory origin) for the baseline and postprandial periods (Figure 2);
(iii) the power ratio (PR) or relative power variation is the ratio of the postprandial to baseline DP values (Figure 3);
(iv) the instability coefficient (IC) was introduced to define the characteristic variation in the DF within the normal range. It is calculated as the standard deviation divided by the mean frequency. A lower IC value will result in a more stable DF.

• Definition of normal EGG
Normal EGG was considered to be present when the percentage of the DF in normogastria was >70% during both periods [37,40,42] and the increase in postprandial power was >15% [35].

Statistical analysis
A descriptive analysis was first conducted using the mean, standard deviation (SD), median, 25th (P25) and 75th (P75) percentiles, and minimum and maximum values. The Kolmogorov-Smirnov test was used to evaluate the probability distribution of the quantitative traits.
FIGURE 1. Multichannel electrogastrography signal analysis. A. EGG waves tracing recorded in bipolar channels; B. EGG waves tracing recorded in monopolar channels; C. Respiratory movements trace channel; D. Fast Fourier transform (FFT) of EGG power spectrum; E. multiple FFT lines - running spectral analysis.

FIGURE 2. Example of traces showing the FFT lines in normal EGG recordings in the baseline and postprandial periods (A and B). The dominant frequency is maintained in the frequency range between two and four cpm.
The hypothesis that the baseline DF and postprandial DF exhibited the same distribution during both periods was tested using a paired t-test. All tests performed used a two-tailed α of 0.05 and a confidence interval (CI) of 95% and were performed with using Statistical Package for the Social Sciences version 25 (IBM Corp. Released 2017. IBM SPSS Statistics for Windows, Version 25.0. Armonk, NY: IBM Corp.).

RESULTS

A total of 20 healthy individuals were evaluated, including 11 (55%; 95%CI=33.8–74.9%) females and 9 (45%; 95%CI=25.1–66.2) males. The mean age of the study subjects was 41±10 years (TABLE 1).

TABLE 1. Descriptive statistics including the demographic data and the outcomes achieved at multichannel electrogastrography.

|                          | Mean±SD | Median (P25-P75) | Minimum-maximum |
|--------------------------|---------|------------------|-----------------|
| Age                      | 41.0±10.0 | 40.0 (34.0–48.0) | 27–68          |
| Fasting dominant frequency | 2.7±0.2   | 2.7 (2.6–2.9)    | 2.4–3.1        |
| Postprandial dominant frequency | 2.9±0.2   | 2.9 (2.8–3.0)    | 2.6–3.2        |
| Power ratio              | 9.5±15.4  | 3.7 (1.9–9.0)    | 0.36–67.0      |
| Overall dominant frequency | 2.9±0.3   | 2.8 (2.6–3.1)    | 2.3–3.3        |
| Normogastria fasting (%) | 87.5±11.8 | 87.3 (77.0–100)  | 70.5–100       |
| Normogastria postprandial (%) | 90.4±9.7  | 91.5 (84.6–100)  | 72.2–100       |
| Dominant frequency instability coefficient fasting | 14.5±5.4 | 15.6 (11.7–17.1) | 2.7–27.2 |
| Dominant frequency instability coefficient postprandial (%) | 11.2±3.5 | 11.6 (8.4–13.5) | 5.7–19.7 |

The mean DF at rest was 2.7±0.2 cpm, and the mean postprandial DF was 2.9±0.2 cpm. The difference of 0.2 cpm was statistically significant (P-value=0.010).

The DF showed little variability (2.9±0.3 cpm). Also, the mean and median percentages of the DF in normogastria in the baseline and postprandial periods were 87.5±11.8 and 90.4±9.7% and 87.3% (77.0–100.0%) and 91.5% (84.6–100.0%), respectively. There was no significant difference between the two periods (P-value=0.116).

The PR exhibited heterogeneity among the subjects, with a mean of 9.5±15.4 and a median of 3.7 (1.9–9.0).

DISCUSSION

With technological advancements over time, the method by which EGG is recorded and its new settings have made the test more reliable[15–17]. For example, the difficulties capturing low amplitude signals and the susceptibility to artifacts have decreased due to technological advances in the technique and as new professionals learn the method[18].

Our study is the first to apply multichannel EGG in the Brazilian population using equipment with new settings, amplifiers, and filters and bipolar electrodes. This greater variety of channels facilitates choosing the best signal among all recordings to represent the optimal measurement of gastric myoelectrical activity[19–21]. One study showed that data obtained with multichannel EGG may provide increased information on gastric myoelectrical activity in patients with suspected motility disorders and in patients with unexplained nausea, vomiting, gastroparesis, and other dyspeptic symptoms[22,23]. EGG also helps to identify the pathophysiology of diseases associated with gastric slow waves or dysrythmia[24,25]. Abnormalities found on EGG have been compared to finding of slow gastric emptying on scintigraphy. Some studies concluded that abnormalities in both tests are present in subsets of patients, but the two tests may define different populations, becoming complementary examinations[26–30].

The variation in the overall DF in our population was 2.3–3.3 cpm, and this range of values is similar to that reported in the literature[24,25,31,32]. The mean DF was also assessed in both periods, and the variation was between 2.6 and 2.9 cpm at baseline and 2.8 and 3.0 cpm postprandial. All individuals in our cohort were healthy volunteers not having any evidence of fasting hyperglycemia or autonomic neuropathy that might interfere with the results observed in this population[33,34]. Rezende Filho et al. (2005) evaluated EGG abnormalities in patients with Chagas disease in Brazil and compared them with a control group of healthy individuals and found mean baseline and postprandial DF variations of 1.17–3.05 cpm and 1.88–2.38 cpm, respectively. However, that study was performed with a single-channel EGG device[35], which is different from our device, which had multiple channels, and may have been a factor in the difference in the results.
Additionally, we observed an increase in the mean DF between the baseline (2.7 cpm) and postprandial (2.9 cpm) periods, and this difference was statistically significant. One study showed that this increase may occur when solid foods are included in the test meal rather than liquid foods only[40].

In the EGG analysis, we observed a high mean percentage of the DF in normogastria (87.5% at baseline and 90.4% postprandial), remaining above 70% in both periods, which is in agreement with the literature.4,35,39,

Another important finding was the PR, as we identified that only one individual did not present a positive response to the test meal, and the other 19 individuals showed a PR greater than 1. A PR <1 may indicate an unsatisfactory stomach motor response to the given stimulus (test meal), and a PR >1 indicates a satisfactory response of the stomach, according to several studies and reviews on the topic.19,21

There is no international consensus on the DF instability coefficient (DFIC). A smaller IC value is known to result in a more stable DF.15. In our study, the DFIC at baseline ranged from 2.7% to 27.2%, and it ranged from 5.7% to 14.5% in the postprandial period, with no significant change after meal ingestion. The literature reports that the DFIC may increase during pregnancy, in patients with gastroesophageal reflux disease14,56, and in patients with clinical improvement after use of prokinetics, which may be due to the increased variability of changes in gastric motility activated by prokinetics57. The power in fasting may possibly vary according to interdigestive electromotor complex, as the recording is only 30 minutes. This may explain variations in the IC and PR.

In conclusion, the use of multichannel EGG in healthy individuals of the Brazilian population, where there is significant miscegenation, yielded data consistent with the literature, thus allowing the application of EGG in future studies evaluating gastric motility disorders in this population.

**References**

1. Leahy A, Besherdas K, Dayman C, Mason I, Epstein O. Abnormalities of the electrogastrogram in functional gastrointestinal disorders. Am J Gastroenterol. 1999;94:1023-8.
2. Alvarez WC, Mahoney LJ. Action currents in stomach and intestine. Am J Physiol. 1922;58:476-93.
3. Davis RC, Garafolo L, Gault FP. An exploration of abdominal potentials. J Comp Physiol Psychol. 1957;50:519-23.
4. Chen JD. Multichannel EGG: principles and applications. Chen JD, Mc Callum RW, editors. New York: Raven; 1994:45-73.
5. Sarno SK. Gastrointestinal Electrical Activity: Terminology. Gastroenterology. 1975;68:1631-5.
6. Kelly KA. Motility of the stomach and gastroduodenal tract. New York: Raven; 1981;393-410.
7. Brown BH, Smallwood RH, Duthie HL, Stodgaard DD. Intestinal smooth muscle electrical potentials recorded from surface electrodes. Med Biol Eng. 1975;97-102.
8. Smout AJPM, Van Der Schee EJ, Grashuis JL. What is measured in electrogastrography? Dig Dis Sci. 1980;33,9.
9. Abell TL, Malagelada JR. Glucagon-evoked gastric dysrhythmias in humans shown by an improved electrogastrographic technique. Gastroenterology. 1985;1392-80.
Transcutaneous multichannel electrogastrography: normal parameters in a Brazilian population

10. Hamilton JW, Bellahsene BE, Reichelderfer M, Webster JG, Bass P. Human electromyograms - Comparison of surface and mucosal recordings. Dig Dis Sci. 1986;33:9.

11. Yin J, Chen JDZ. Electrogastrography: Methodology, validation and applications. J Neurogastroenterol Motil. 2013;19:5-17.

12. Lin Z, Chen JDZ, Schirmer BD, McCallum RW. Postprandial response of gastric slow waves: Correlation of serosal recordings with the electrogastrogram. Dig Dis Sci. 2000;45:645-51.

13. Mintchev MP, Kingma YJ, Bowes KL. Accuracy of cutaneous recordings of gastric electrical activity. Gastroenterology. 1993;127:80.

14. Krusiec-Swidergol B, Jonderko K. Multichannel electrogastrography under a magnifying glass - An in-depth study on reproducibility of fed state electromyograms. Neurogastroenterol Motil. 2008;625-34.

15. Lin X, Chen JZ. Abnormal gastric slow waves in patients with functional dyspepsia assessed by multichannel electromyograph. Am J Physiol Gastrointest Liver Physiol. 2001;1370-5.

16. Sha W, Parshica PJ, Chen JDZ. Correlations Among Electrogastrogram, Gastric Dismotility, and Duodenal Dismotility in Patients With Functional Dyspepsia. J Clin Gastroenterol. 2009;43:716-22.

17. Camilleri M, Hasler WL, Parkman HP, Puglial EMM, Soffer E. Measurement of gastrointestinal motility in the GI laboratory. Gastroenterology. 1998;114:747-62.

18. Qian LW, Pasricha PJ, Chen JDZ. Origins and patterns of spontaneous and drug-induced canine gastric myoelectrical dysrhythmia. Dig Dis Sci. 2003;48:508-15.

19. Chen JD, Schirmer BD, McCallum RW. Serosal and cutaneous recordings of gastric myoelectrical activity in patients with gastroparesis. Am J Physiol. 1994;266:908-9.

20. Chang FY. Electrogastrography: Basic knowledge, recording, processing and its clinical applications. J Gastroenterol Hepatol. 2005;20:502-16.

21. Chen JD, Zou X, Lin X, Ouyang S, Liang J. Detection of gastric slow wave propagation from the cutaneous electromyograph. Am J Physiol. 1999; 277:424-30.

22. Chen JD, Co E, Liang J, Pan J, Stuphen J, Torres-Pinedo RB, Orr WC. Patterns of gastric myoelectrical activity in human subjects of different ages. Am J Physiol Gastrointest Liver Physiol. 1997;272:1022-7.

23. Koch KL, Hong SP, Xu L. Reproducibility of gastric myoelectrical activity and the water load test in patients with dysmotility-like dyspepsia symptoms and in control subjects. J Clin Gastroenterol. 2000;31:125-9.

24. Parkman HP, Hasler WL, Barnett JL, Eaker EY. Electrogastrography: A document prepared by the gastric section of the American Motility Society Clinical GI Motility Testing Task Force. Neurogastroenterol Motil. 2003;15:89-102.

25. Yin J, Chen JDZ. Electrogastrography: Methodology, Validation and Applications. J Neurogastroenterol Motil. 2013;19:5-17.

26. A computerized data anaylsis system for electromyogram. Comput Biol Med. 22:45-57.

27. Rizzuto G, Russo F, Indrio F. Electrogastrography in adults and children: the strength, pitfalls, and clinical significance of the cutaneous recording of the gastric electrical activity. BioMed Res Int. 2013;282:75.

28. Mintchev MP, Bowes KL. Extracting quantitative information from digital electromyograms. Med Biol Eng Comput. 1996;34:248-8.

29. Chen JD, McCallum RW. Clinical applications of electromyograph. Am J Gastroenterol. 1993;88:1324-36.

30. Chen J, McCallum RW. Gastric slow wave abnormalities in patients with gastroparesis. Am J Gastroenterol. 1992;87:477-82.

31. Pfaffenbach B, Adamek RJ, Kuhn K, Wegener M. Electrogastrography in healthy subjects. Dig Dis Sci. 1995;40:1445-50.

32. Lin Z, Eaker EY, Sarosiek I, McCallum RW. Gastric myoelectrical activity and gastric emptying in patients with functional dyspepsia. Am J Gastroenterol. 1999;94:2384-9.

33. O’Grady G, Abell TL. Gastric arrhythmias in gastraparesis: low- and high-resolution mapping of gastric electrical activity. Gastroenterol Clin North Am. 2015;44:169-84.

34. Chen J, McCallum RW. Effect of milk on myoelectrical activity of the stomach— an electromyographic study. Med Biol Eng Comput. 1992;30:564-7.

35. Geldof H, Van Der Schee EJ, Van Blankenstein M, Grashuis JL. Electrogastrographic study of gastric myoelectrical activity in patients with unexplained nausea and vomiting. Gut. 1986;250:165-71.

36. Smen J, Casariego M, Panagianama T, Han JZ, Fisher RS, Parkman HP, Multichannel electrogastrography (EGG) in symptomatic patients: a single center study. Am J Gastroenterol. 2004;99:478-485.

37. Bertolotti M, Sarti P, Barbara L, Brunelli F. Gastric Myoelectric Activity in Patients with Chronic Idiopathic Gastroparesis. Neurogastroenterol Motil. 2005;17:104-8.

38. Chen JD, Lin Z, Pan J, McCallum RW. Abnormal gastric myoelectrical activity and delayed gastric emptying in patients with symptoms suggestive of gastroparesis. Dig Dis Sci. 1996;41:1538-45.

39. Parkman HP, Miller MA, Trate D, Knight LC, Urbain JL, Maurer AH, Fisher RS. Electrogastrography and gastric emptying scintigraphy are complementary for assessment of dyspepsia. J Clin Gastroenterol. 1997;24:214-9.

40. You CH, Lee KY, Chey WY, Menguy R. Electrogastrographic study of patients with unexplained nausea, bloating, and vomiting. Gastroenterol. 1980;79:311-4.

41. Couturier D, Rozé C, Paolaggi J, Debray C. Electrical activity of the normal human stomach. Am J Dig Dis. 1972;17:969-76.

42. Geldof H, van der Schee EJ, Grashuis JL. Electrogastrographic characteristics of interdigestive migrating complex in humans. Am J Physiol. 1986;250:G165-71.

43. Hasler WL, Soudah H.C, Dulai G., Owyang C. Mediation of Hyperglycemia-Evoked Gastric Slow-Wave Dysrhythmias by Endogenous Prostaglandins. Gastroenterology. 1995:108:727-36.

44. Jepbink HJA, Bruips PPM, Bravenboer B, Akkermans LMA, Smout AJP. Gastric myoelectrical activity in patients with type I diabetes mellitus and autonomic neuropathy. Dig Dis Sci. 1994;39:2376-83.

45. Parkman HP, Harris AD, Miller MA, Fisher RS. Influence of age, gender, and menstrual cycle on the normal electromyogram. Am J Gastroenterol. 1996;91:127-33.

46. Rizzuto G, Pezzolla F, Darconza G, Giorgio I. Gastric Myoelectrical Activity in Patients with Functional Dyspepsia. J Clin Gastroenterol. 2002;22:45-57.

47. Lim HC, Lee SI, Chen JDZ, Park H. Electrogastrography associated with somatic changes after prokinetic drug treatment for functional dyspepsia. World J Gastroenterol. 2012;18:5948-56.