Visualization, imaging and new preclinical diagnostics in radiation oncology

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Abstract

Innovative strategies in cancer radiotherapy are stimulated by the growing knowledge on cellular and molecular tumor biology, tumor pathophysiology, and tumor microenvironment. In terms of tumor diagnostics and therapy monitoring, the reliable delineation of tumor boundaries and the assessment of tumor heterogeneity are increasingly complemented by the non-invasive characterization of functional and molecular processes, moving preclinical and clinical imaging from solely assessing tumor morphology towards the visualization of physiological and pathophysiological processes. Functional and molecular imaging techniques allow for the non-invasive characterization of tissues in vivo, using different modalities, including computed tomography (CT), magnetic resonance imaging (MRI), ultrasound, positron emission tomography (PET) and optical imaging (OI). With novel therapeutic concepts combining optimized radiotherapy with molecularly targeted agents focusing on tumor cell proliferation, angiogenesis, and cell death, the non-invasive assessment of tumor microcirculation and tissue water diffusion, together with strategies for imaging the mechanisms of cellular injury and repair is of particular interest. Characterizing the tumor microenvironment prior to and in response to irradiation will help to optimize the outcome of radiotherapy. These novel concepts of personalized multi-modal cancer therapy require careful pre-treatment stratification as well as a timely and efficient therapy monitoring to maximize patient benefit on an individual basis. Functional and molecular imaging techniques are key in this regard to open novel opportunities for exploring and understanding the underlying mechanisms with the perspective to optimize therapeutic concepts and translate them into a personalized form of radiotherapy in the near future.

Keywords: Radiation oncology, Molecular imaging, Functional imaging, Preclinical models

Introduction

The effective use of radiation for cancer treatment is closely linked to the optimal application of imaging for staging and tumor characterization. Therefore any improvement in the field of imaging will impact on radiation oncology per se. In a broader sense the term imaging may not only be used to cover aspects of patho-anatomical imaging but may also cover all relevant aspects of additional functional visualization. The growing knowledge on the pathophysiology of cancer and the associated paradigm shift in therapeutic concepts are moving preclinical and clinical imaging from exclusively assessing tumor morphology towards the visualization of physiological and pathophysiological processes on a molecular level. Functional and molecular imaging allows for the non-invasive characterization of tissues in vivo, and comprises techniques, such as computed tomography (CT), magnetic resonance imaging (MRI), ultrasound, positron emission tomography (PET) and optical imaging (OI). These novel imaging techniques have the potential for the visualization of functional tumor properties and the quantification of molecular pathways regulating the hallmarks of cancer [1]. As such, signaling pathways orchestrating proliferation, survival, angiogenesis, invasiveness, metastasis, and different types of cell death can be visualized either directly or indirectly via surrogate markers [2]. Imaging the mechanisms of cellular injury, repair, and cell death is of particular interest for characterizing the tumor microenvironment prior to and in response to

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irradiation, and hence for optimizing the outcome of radiotherapy (RT) [3].

RT is an established, highly effective cancer treatment option applied for definite, curative treatment as well as for palliative care. Together with surgery and/or chemotherapy it is an integral part of multimodality approaches. Novel therapeutic concepts include optimized radiotherapy in combination with molecularly targeted agents focusing on tumor cell proliferation, angiogenesis, and cell death [4]. Importantly, these concepts require predictive biomarkers in order to stratify tumors for the appropriate therapy according to their individual molecular profile as well as biomarkers for monitoring the therapeutic outcome on a non-invasive and serial basis in vivo. E.g. with regard to tumor heterogeneity, the non-invasive evaluation of cellular tumor properties, such as proliferation, using molecular imaging methods could be of great interest for radiotherapy planning, for the identification of highly proliferative tumor areas. Functional and molecular imaging techniques may be key in this regard, since they open novel and exciting opportunities for exploring the molecular mechanisms in radiation biology with the possibility to optimize therapeutic concepts and translate them into a personalized form of radiotherapy in future.

Imaging modalities

Computed Tomography (CT)

CT is one of the leading imaging modalities in medical imaging and standard-of-care in RT planning. Advantages include short examination times allowing for whole body imaging within seconds, broad availability of the technique as well as low costs. Additionally, CT offers high spatial resolution at the submillimeter level. In small animal imaging, morphologic micro CT has shown significant potential with benefits, including high throughput and superior resolution. Winkelmann and colleagues investigated micro CT in a bone metastasis model of prostate cancer in mice and found that bone micro CT was able to non-invasively follow the onset and progression of bone metastatic lesions as small as 300 μm in diameter [5]. Although radiation dose per micro CT scan approached 7–9 cGy, with six to nine micro CT examinations per mouse over a 7-week period, the applied radiation dose did not induce tumor stasis. However, the radiation dose applied by diagnostic micro CT has to be taken into account, particularly, when investigating micro CT for RT planning in small animal tumor models. A study by Boll and colleagues [6] investigated a dedicated alkaline earth metal-based nanoparticulate contrast agent for micro CT imaging of liver metastases in a colon carcinoma metastasis model in mice and reported that liver metastases as small as 300 μm were detectable after a single injection. The authors concluded that the investigated nanoparticulate contrast agent is suitable to compensate for the limited soft tissue contrast of unenhanced micro CT and allows for high resolution and high soft tissue contrast imaging of tumors in small animal models. Therefore, micro CT enhanced with dedicated contrast media may be of particular interest for the delineation and non-invasive characterization of tumors before and during radiotherapy in the preclinical setting.

Recent studies also support the value of perfusion CT as a functional imaging method in oncology [7]. Perfusion imaging techniques based on CT, MRI and ultrasound have been applied for the non-invasive quantification of functional parameters of tissue microcirculation [8-11]. It has also been shown that dynamic contrast-enhanced CT (DCE-CT) allows for the assessment of pathologically increased tissue perfusion, blood volume and permeability [12], reflecting typical features of angiogenically active tissues, such as tumors. Surrogate parameters of tumor microcirculation assessed by DCE-CT have the potential to predict response to chemotherapy or irradiation in various cancers, e.g. cancers of the head and neck, lung, and rectum [13-15]. In anti-angiogenic tumor therapy, DCE-CT has shown its applicability for early assessment of the therapeutic effect on tumor vascularization, identifying treatment responders from non-responders, and optimizing personalized molecular therapies on an individualized patient basis.

Dual-energy CT (DECT) offers high soft tissue contrast and a clear differentiation between soft tissue, iodine contrast and bone. Dual source DECT can provide iodine maps which reflect iodine content in a tissue of interest and which have been demonstrated to show good correspondence to perfusion images in the lung and heart [16,17]. In an experimental study of a VX2-rabbit model of liver cancer Zhang and colleagues reported that DECT iodine maps correlated well with multiparametric perfusion CT measurements for monitoring tumor angiogenesis with a significantly lower effective radiation dose. It was concluded that DECT might have the potential for serially monitoring angiogenesis in solid tumors with a significant reduction in radiation dose compared to perfusion CT techniques [18]. This technique may be of particular interest for serially monitoring tumor heterogeneity and angiogenesis in the planning and monitoring of RT combined with anti-angiogenic agents.

Magnetic Resonance Imaging (MRI)

Based on strong magnetic fields (clinically between 1.5 and 3 Tesla, human research scanners up to 7 Tesla) MRI is able to provide superior soft tissue contrast and high spatial resolution without the application of ionizing radiation. Besides its morphologic capabilities useful for clinical staging and RT planning purposes [19,20], MRI is increasingly developed for functional and molecular imaging methods,
among them perfusion and diffusion imaging as well as MR spectroscopy and molecular MRI. Perfusion MRI can be applied to quantify functional parameters of tissue microcirculation, which have been shown to reflect tissue properties such as vitality, angiogenesis and proliferation [21]. Novel imaging methods such as 23Na MRI have been proposed as a potential imaging biomarker for the assessment of tumor viability and the evaluation of therapy response in cancer patients [22].

**Magnetic Resonance Proton Spectroscopy (MRS)**

MR spectroscopy uses selective radiofrequency pulses for the investigation of the molecular composition of tissues [23,24]. The Fourier transformation of the acquired signal generates a defined spectrum allowing for the discrimination of different metabolites in the investigated tissue, which may be pathognomonic for certain underlying pathologies. Metabolites detected in tumor tissues include choline-containing compounds, creatine, glutamate, lactate, N-acetyl aspartate (NAA), myoinositol (mI) and taurine [25]. The concentration of each of these metabolites can be mapped on spectroscopic images with a voxel size of 0.7-1 cm³. NAA is predominantly a neuronal marker and decreases associated with neuronal damage and dysfunction [25]. Choline is associated with cell membrane synthesis as well as increased metabolic turnover and is elevated in tumors and inflammatory processes [25]. Creatine has been shown to be a marker of energy metabolism in the brain [26], while mI was confirmed as a glial cell marker and has been used as an indicator of myelin breakdown [27]. In glioblastomas increased levels of creatine and choline as well as a lowered level of N-acetyl aspartate were found [28]. Additionally, MRS can be applied for pre-operative staging of gliomas [29] and for monitoring tissue pH and temperature [30]. With regard to radiation therapy, MRS may be a sensitive tool for monitoring radiation-induced changes in tumors based on the acquired spectrum of metabolites. MRS has also been postulated to be of particular interest in focal dose escalation in prostate cancer patients [31]. Significant technical challenges for clinical translation remain particularly with regard to reproducibility in the quantification of chemical metabolites in tumors as well as impeded data quality due to local-field inhomogeneities caused by healthy tissue adjacent to the tumor [26].

**MR perfusion**

MR perfusion represents one of the most promising methods of functional MR imaging. Perfusion imaging is defined as the *in vivo* assessment and quantification of microcirculatory parameters in different tissues, which may allow for the characterization of an underlying pathology. Depending on the imaging protocol and kinetic models applied for data analysis different parameters of microcirculation, such as plasma flow, extraction fraction, or relative plasma volume, can be assessed reflecting tissue properties, such as tissue perfusion, endothelial permeability, and tissue vascularity [32], *in vivo*. Technically, MR perfusion imaging can be performed by dynamic contrast-enhanced imaging (DCE), dynamic susceptibility contrast imaging (DSC), and arterial spin labeling (ASL) techniques. The most common method for perfusion imaging, however, is dynamic contrast-enhanced imaging.

Methodologically, DCE imaging monitors signal enhancement before, during and after intravenous injection of a paramagnetic contrast agent applying T1-weighted sequences with high temporal and spatial resolution [21]. The resulting signal-intensity vs. time curve can be analyzed to yield different quantitative and semi-quantitative parameters, for example maximum signal enhancement, time-to-peak, maximum slope or area under the curve. These semi-quantitative parameters describe important aspects of contrast media kinetics and can be routinely assessed with high robustness. However, physiological interpretation of these semi-quantitative parameters is often difficult [33] and factors like acquisition time, temporal resolution, sequence parameters, contrast media dose, and bolus velocity greatly influence semi-quantitative parameters. As a consequence, semi-quantitative parameters are only of limited use for follow-up measurements and multicenter studies. As demonstrated in Figure 1, DCE-MRI can also be applied for the assessment of quantitative parameters of tissue microcirculation, such as plasma flow (ml/min/100 ml), extraction flow (ml/min/100 ml), and plasma volume (%) [34]. These parameters are considered to be physiologically distinct with better suitability for longitudinal and multicenter studies, but strongly depend on standardized imaging and analysis protocols. Depending on the kinetic profile of the contrast medium, investigated tissue of interest and acquisition technique a range of kinetic models is available for the analysis of the kinetic data, e.g. the Patlak or the Tofts model [35]. The best model to fit the data can be evaluated using the Akaike’s information criterion, which can be applied to support model selection for the mathematical description of tracer kinetics [36]. Clinically, MR perfusion imaging has great potential as a functional imaging method in oncology for the assessment of tumor vitality, angiogenesis, and tumor heterogeneity. In e.g. prostate cancer, it can be used after radical prostatectomy to detect local recurrence without an endorectal coil [37], for therapy response imaging [38] as well as for the determination of extracapsular extension [39]. However, standardization of acquisition protocols and data analysis remain major obstacles towards broader establishment of the technique in clinical routine [21].
MR diffusion imaging is another major technique of functional MR imaging and is already routinely applied in neuroradiologic imaging protocols. In MR diffusion imaging, gradient pulses generate a spatially varying magnetic field with resulting phase differences of the MR signal, which are caused by the random motion of water molecules in the tissue (Brownian motion). Diagnostic applications of MR diffusion imaging include ischemia [40], tumor diagnosis and characterization [41], multiple sclerosis [42], therapy response assessment [38] as well as fiber tracking using diffusion tensor imaging (DTI). Recent studies have also investigated the potential of diffusion imaging for therapy monitoring [43] and the assessment of biomarkers in oncology with promising results [41]. In this context, Somford and colleagues successfully investigated DWI for the identification of high-grade prostate carcinoma in patients with a Gleason score $\geq 3 + 3 = 6$ after TRUS-guided biopsy and concluded that DWI is able to predict the presence of high-grade tumor with significant relevance for subsequent treatment decisions. In a study of 73 patients with prostate cancer, Ueno et al. found that diffusion-weighted MRI with ultra high b-values ($b = 2000 \text{ s/mm}$) is superior compared to the use of high b-values ($b = 1000 \text{ s/mm}$) for prostate cancer detection, validated by histopathology following radical prostatectomy [44]. These ultra-high b-values may be assessable by computed DW MRI, as shown in a study by Blackledge and co-workers, who investigated DW MR imaging in 10 oncologic patients with b values of 0 and 900 sec/mm, subsequently generating images with computed b values of 1500 and 2000 sec/mm. They found that images with a computed b value of 2000 sec/mm resulted in higher overall diagnostic sensitivity and specificity compared to images with an acquired b value of 900 sec/mm [45]. A novel application of MR diffusion is intravoxel incoherent motion (IVIM) imaging, which allows to derive quantitative parameters that reflect tissue microcapillary perfusion and tissue diffusivity [46]. A bi-exponential model is fitted to diffusion-weighted data, to quantify the measured signal attenuation as a function of diffusion (b-value). Perfusion information is extracted from the initial signal attenuation at low b-values between 0 and ca. 150 s/mm$^2$ [46]. Figure 2 shows a representative example of a subcutaneous tumor xenograft of head and neck squamous cell carcinoma in rats imaged by diffusion-weighted MRI with voxel-wise analysis using the bi-exponential IVIM model. Several recent studies have also discussed a possibly enhanced diagnostic value of multiparametric MRI combining morphologic and functional information from perfusion and diffusion parameters for the non-invasive characterization and differentiation of tumors [47]. The recently published guidelines of the European Society of Urogenital Radiology (ESUR) describe the application of multiparametric MRI for the detection and staging of prostate cancer, a separate protocol for node and bone imaging as well as a standardized reporting system (PI-RADS), analogue to breast imaging [48].

**Figure 1** Representative axial T1 weighted TWIST image of an athymic rat bearing a subcutaneous colon carcinoma xenograft over the left flank. (a) Representative axial T1 weighted TWIST image of an athymic rat bearing a subcutaneous colon carcinoma xenograft over the left flank with the arterial input function (AIF) measured in the inferior vena cava as well as the signal enhancement curve over the tumor. (b) Representative quantitative parameter maps depicting different parameters of tumor microcirculation (from top to bottom): plasma volume (%), plasma flow (ml/100 ml/min), plasma mean transit time (s), permeability surface area product (ml/100 ml/min).
mMRI applies targeted, gadolinium- or iron-based contrast agents of different designs, which allow for the dedicated depiction of molecular processes in vivo using antibodies, peptides or peptidomimetics [49,50]. Based on Gadolinium (Gd) or iron, these contrast agents cause a shortening of the T1- (Gd) or the T2/T2* time (iron) and lead to a change in tissue contrast. To achieve highly specific binding properties, Gd-chelates or nanoparticles are conjugated to antibodies, peptides or peptidomimetics for the dedicated in vivo visualization of molecular processes [50]. Serres and co-workers developed a targeted MRI contrast agent based on iron oxides that enables imaging of endothelial vascular cell adhesion molecule-1 (VCAM-1), which is known to be up-regulated on vessels of cerebral metastases [51]. They investigated whether MRI enhanced with the targeted anti-VCAM-1 microparticles of iron oxide (anti-VCAM-1 MPIO) would be able to depict up-regulated VCAM-1 in a model of human breast carcinoma cerebral metastasis in mice and if early detection of these metastases would be feasible. The results indicated that by use of the VCAM-1 targeted MRI contrast agent, it is possible to detect brain metastases substantially earlier than with the established gadolinium-based small molecular contrast media and concluded that this approach represents a highly sensitive method for the early detection of brain metastases with the potential for clinical translation [51].

**Hyperpolarized MRS**

Compared to the currently established proton-based MR imaging, other nuclei like $^3$He, $^{129}$Xe or $^{13}$C have lower occurrence in the human body. If these alternative nuclei were used for the generation of the radiofrequency signal in MRI, the resulting signal-to-noise ratio (SNR) would be quite low. By means of hyperpolarization, however, it is possible to excite specific nuclei, thereby potentiating their MR signal to achieve a better SNR. $^3$He und $^{129}$Xe can be polarized by optical pumping, while $^{13}$C can be polarized using parahydrogen and dynamic polarization [53]. Different studies have investigated $^{13}$C in MR angiography- and perfusion studies as well as $^{129}$Xe for lung imaging [54,55]. Experimental, hyperpolarized MR contrast agents such as $^{13}$C-urea do not alter relaxation time, as established Gd- or iron based MR contrast media, but resemble in their function radioactive tracers, with the hyperpolarized nuclei representing the basis for the MR signal.

To date, $^{13}$C pyruvate has been the most widely used hyperpolarized substrate for MRS, which has also been applied for tumor response monitoring [56], and was the first to be used in a clinical trial of the technique [57]. In a study investigating the effects of the mTOR inhibitor everolimus on a highly invasive orthotopic glioblastoma model in rats. Chaumeil and colleagues demonstrated that hyperpolarized $^{13}$C MRS can be used on a clinical MR system to monitor early metabolic response by means of measurement of the HP lactate-to-pyruvate ratios [58]. Similarly, Day et al. showed the applicability of hyperpolarized $^{13}$C pyruvate MRS for the detection of treatment response 72 h following a whole brain
Ultrasound

In recent years, ultrasound has undergone significant technological advancement with an evolution from a simple morphology-based gray-scale image to a multi-parametric high-resolution real-time imaging system. Major developments include the introduction of functional imaging options including sophisticated Doppler ultrasound, contrast-enhanced ultrasound (CEUS), and elastography for the non-invasive characterization of tissues with significantly improved spatial and temporal resolution. The development of gas-filled blood-pool microbubble contrast agents has significantly enhanced clinical and pre-clinical research applications with particular regard to the in vivo characterization of tissue microcirculation in a semi-quantitative and quantitative manner [63]. Novel targeted microbubble contrast agents available for research purposes open the door for a molecular evaluation of tissues, e.g. by selectively binding to vascular endothelial growth factor receptor (VEGFR-2) [64-68] and a possible theranostics application linked to high intensity focused ultrasound (HIFU) which may be used in recurrent prostate cancer [69] and the microbubble-assisted delivery of drugs and genes [70].

Clinically, in recent years image-guided radiotherapy has been a major issue in research and development for (mage-guided radiotherapy (IGRT) and may be regarded as standard-of-care, especially in high-precision radiotherapy. One newly developed system is based on ultrasound – the Clarity 3D™ ultrasound system (Elekta, Stockholm, Sweden) is designed to track exemplarily the prostatic gland and adjacent organs-at-risk in order to minimize setup errors caused by organ motion, displacements and different filling states [71]. Furthermore, ultrasound has great potential to be established as a sensor for intrafractional movement as the tumor or organ motion can be tracked online as compared to a static cone beam CT (pre or post application of the individual fraction), e.g. in liver cancer/metastases or prostate cancer [72]. This in turn allows for an early detection of significant deviations and could in principle be used for real tumor tracking during irradiation.

**Contrast-enhanced sonography (CEUS)**

In CEUS, gas-filled microbubbles are injected intravenously, thereby creating a multitude of small interfaces with high echogenicity. After destruction, the gas (e.g. SF\textsubscript{6}) is eliminated over the lungs within minutes and phospholipid membranes will be endogenously metabolized. The diameter of most microbubbles ranges between 2–10 μm, quite similar to the diameter of erythrocytes. Contrary to conventional small molecular CT- and MRI- contrast media, the microbubbles do not extravasate into the interstitial space, remain intravascular and therefore belong to the class of blood pool contrast media [73,74]. Microbubbles oscillate and vibrate resulting in a continuous improvement of gray scale contrast. With the development of high-frequency linear ultrasound transducers (>20 MHz) ever-smaller structures can be examined by CEUS with superior temporal and spatial resolution (Figure 3).

For the most part CEUS has been applied for investigations of tumors in parenchymatous organs and in pathologies of the vascular system [75–83], where CEUS can be applied as a functional imaging method for the assessment of tissue microcirculation in healthy and malignant tissues. CEUS perfusion imaging may be particularly attractive for monitoring novel, molecular therapies in oncology mainly targeting tumor angiogenesis [84]. Paprottka and co-workers showed in an experimental study that CEUS allows for superior assessment of tumor perfusion compared to color-coded duplex ultrasound and power Doppler [84]. Other preclinical studies demonstrated that parameters of tumor microcirculation assessed by CEUS may be applicable as imaging biomarkers of tumor angiogenic activity and may have the potential to be used as non-invasive biomarkers of tumor responses under anti-angiogenic therapy (Figure 4) [85,86]. Radiotherapeutic applications of CEUS include treatment guidance in prostate brachytherapy planning [87] and it has a potential role in monitoring of liver metastases after stereotactic radiosurgery [88].

Apart from non-targeted, blood-pool ultrasound contrast media, targeted microbubbles have been developed as a molecular imaging technique by attaching specific ligands to the coating of gas-filled microbubbles. These targeted microbubbles can be applied for the non-invasive characterization of molecular tissue properties in vivo. As ultrasound microbubble contrast media remains intravascularly after intravenous injection, molecular targets have to be located on the luminal surface of vascular...
endothelium. Targeted microbubbles have been conjugated to ligands specific for highly expressed molecular markers of tumor angiogenesis such as VEGFR-2 and αvβ3-integrin [64,65,68,70] to allow for the assessment of tumor angiogenic activity and for monitoring anti-angiogenic therapies in preclinical tumor models [90-92]. Together with potential application in theranostics multiparametric, contrast-enhanced ultrasound has developed to a high-potential tool for research and patient care combining high sensitivity, real-time morphological imaging, with functional and molecular imaging options with a lack of ionizing radiation and at comparably low costs [93].

**Elastography**

Tissue elastography complements the conventional B-image, color Doppler, and CEUS in the assessment of pathologies [94,95]. Ultrasound elastography bridges the gap between modern state-of-the-art ultrasound and one of the most ancient examination techniques in medicine – palpation. Tissue elasticity is frequently altered in the presence of inflammation or malignancy and can be detected by compression elastography on the basis of compression and release [96]. Malignancies frequently exhibit higher tissue stiffness due to high rates of cell proliferation and densely packed cells. Thus, they appear

Figure 3 Contrast-enhanced ultrasound (CEUS) with intravascular SF₆-filled microbubbles: online quantification of hypervascular tumor tissue (turquoise ROI), tumor necrosis (yellow ROI) and feeding vessels (red ROI).

Figure 4 Offline absolute quantification of perfusion of the whole tumor and hypervascular tumor parts using the flash replenishment method [89]. ROIs can be drawn in different parameter maps, allowing a simpler and more standardized analysis of the digitally stored video sequences.
less elastic in ultrasound elastography. By means of the combined autocorrelation method, elastic tissue properties of different tissues can be assessed (Figure 5). Application of light pressure on the tissue with the ultrasound probe and the subsequent release aid to assess relative stiffness of the investigated tissue and differences can be visualized, either in gray scale or color coded, parallel, or merged with a conventional b-image (Figure 6). Several studies investigated ultrasound elastography in mammography as well as in liver and prostate imaging and found that elastic tissue properties contribute valuable information, which is not discriminable in conventional ultrasound [97-101]. In an animal study elastography was applied to monitor ethanol injections for the treatment of liver tumors, and the authors concluded that elastography added significant information compared to the conventional b-image [102,103]. After adjuvant radiotherapy of breast cancer, elastography can be used to quantify the extent of lymph edema [104].

Optical imaging
Optical imaging employs light for the assessment of functional and molecular tissue information. This light can either originate from administered, elicited fluorescent tracers or – as bioluminescence – from genetically modified cells [105]. Upon excitation with externally applied light of the proper wavelength, fluorescent tracers emit light with a higher wavelength that can be detected by a CCD (charged-coupled device) camera. Different forms of tracers have been described. For visualization of blood flow, unspecific, blood-flow distributing agents can be used, much resembling established contrast agents for x-ray computed tomography or magnetic resonance tomography [106]. For visualization of molecular processes, targeted probes have been designed, typically consisting of a fluorescent dye (e.g. Cy 5.5) and a binding moiety – e.g. an antibody or smaller peptide with binding specificity for the target of interest. To minimize tissue absorption and scattering of the emitted light, the optimal spectral range for in vivo applications has been defined as the near-infrared optical window (wavelengths 650–900 nm), with lowest tissue absorbance for hemoglobin, water and lipids. In bioluminescence, an in vivo enzymatic reaction is responsible for the emission of light. The most common enzymatic tool is the firefly luciferase system, where D-luciferine is oxidized using ATP (adenosine-tri-phosphate) and oxygen in a two-step mechanism. The resulting emission of yellow-green light at 575 nm can be employed to visualize luciferase-expressing cells in vivo following intravascular injection of D-luciferine, the substrate of firefly luciferase, or after providing D-luciferine in the drinking water. Advantages of bioluminescence imaging include (1) an exquisite imaging sensitivity due to a high signal-to-noise ratio caused by the lack of bioluminescence background signal (in mammals) and (2) the luciferase system does not require excitation light from outside to be activated. Disadvantages include the need for cell transfection with the luciferase reporter genes, substrate injection (D-luciferine), and the poor spatial resolution of bioluminescence imaging compared to tracer-mediated fluorescence optical imaging. In recent years, many studies have investigated the luciferase bioluminescence assay to visualize a wide array of molecular pathways for the non-invasive characterization of the tumor microenvironment as useful tools in radiation and cancer biology research.

Bioluminescence optical imaging using firefly luciferase has been applied to image an array of biological pathways and cellular processes relevant for novel approaches in radiation and molecular cancer therapy [107]. In a recent study, Li and colleagues developed an imaging system for non-invasive quantification of epidermal growth factor receptor (EGFR) activation in vivo.
based on the bi-fragment luciferase reconstitution system. Epidermal growth factor and its receptor are part of a key-signaling cascade responsible for the initiation and growth of malignancies. Li and colleagues fused the EGF receptor and its interacting partner proteins growth factor receptor binding protein 2 (grb2), and Src homology 2 domain-containing protein (shc) to the amino-terminal and the carboxyterminal fragments of the firefly luciferase, respectively. In this system, firefly luciferase is only enzymatically active when the two parts of the protein are brought together, hence when EGFR, and grb2 or EGFR and shc are interacting and the signaling cascade is active. With the help of this system EGF-induced as well as radiation-induced pathway activation could be convincingly measured in vitro and in vivo (Figure 7) [108]. Moreover, this system was employed to visualize hyperthermia-induced EGFR activation in tumor cells and the potential mechanisms involved [109]. In an analogue study, Li and colleagues utilized their split-luciferase system in order to quantitatively assess DNA double strand breaks and their repair [110]. They fused the N- and C-terminal fragments of firefly luciferase with H2AX and MDC1, two proteins, which at the sites of DNA double strand breaks physically interact with each other. Hence, upon generation of DNA double strand breaks, the two luciferase fragments are brought together and luciferase activity can be detected at the site of damage. Since DNA double strand breaks and the mechanisms of their repair are of crucial interest in the context of ionizing radiation, this imaging system is of specific relevance for monitoring the effect of radiotherapy in tumor tissue.

The study of Backer and colleagues exemplary illustrates strengths and drawbacks of targeted optical imaging with near-infrared fluorescent tracers. Human vascular endothelial growth factor (VEGF) was labeled with the fluorescent dye Cy5.5 (emission maximum 696 nm) for application in an in vivo tumor model [111]. The elevated contrast, observed in the tumor following tracer administration was assigned to elevated VEGFR expression on tumor cells and adjacent endothelia. Unfortunately, the question remained unanswered, how specific this accumulation was. The authors missed to provide data on essential parameters, including whole

**Figure 7** Mice implanted with EGFR-luc transfected H322 tumors over the right flank. EGFR activation during radiotherapy (B, C; 3x6Gy) induces consecutive Luciferase expression and thus detectable bioluminescence upon luciferine injection. Mice implanted into the right flank with EGFR-luc transfected H322 tumors. EGFR activation during radiotherapy (B, C; 3x6Gy) induces consecutive Luciferase expression and thus detectable Bioluminescence upon Luciferine injection. Changes to the EGFR activation by EGFR inhibition with e.g. Gefitinib (C) result in detectable alterations of the signal. Non-treated tumors (A) do not exhibit a specific signal. Adapted by permission from the American Association for Cancer Research: Li et al., Noninvasive imaging and quantification of epidermal growth factor receptor kinase activation in vivo. Cancer Research, 2008, 68, 4990–7. [109].
body distribution of the tracer or an unspecifc control of equal size and distribution. Importantly, biodistribution studies and blocking experiments are a crucial requirement for such imaging studies in order to convincingly show that tracer-mediated fluorescence in fact is a reliable measure of tracer to target binding.

Mostly due to restricted penetration depth of light and strong scatter, clinical translation of optical imaging techniques seems to be limited to lesions in or close to the skin, lesions accessible by endoscopy (e.g. colon polyps), or intraoperative applications. To solve some of these limitations, current technical developments in optical imaging focus on scanners with improved penetration depth and sensitivity, including photoacoustic imaging systems as well as hybrid fluorescence molecular tomography x-ray computed tomography scanners (FMT-XCT) [112-114]. The application of either or both technologies will help to provide significant insights into the molecular mechanisms of radiation and tumor biology in vivo. However, even state of the art optical imaging is a valuable modality for preclinical imaging in small animals, allowing for the non-invasive characterization of cells and tissues on a molecular level. The use of highly specific tracers or reporter gene-based bioluminescence imaging systems will help to gain a better understanding of the molecular processes, which take place in tumors in response to irradiation and/or targeted therapy, and will finally result in a more efficient pretherapeutic stratification of tumors for multimodal therapy.

**Positron emission tomography (PET)/single photon emission computed tomography (SPECT)**

PET is a non-invasive imaging technique that visualizes the distribution and accumulation of positron-emitting tracers in the whole body with high sensitivity providing functional and molecular information on tissues. With its high sensitivity for radiotracers even in picomolar amounts, PET allows for excellent depiction of specific metabolic activity, molecules and receptors in vivo. Besides the established 18 F-fluorodeoxyglucose (FDG), a broad spectrum of PET tracers is under development for the non-invasive imaging of cellular processes such as angiogenesis, proliferation and hypoxia (Table 1). DOTA-TATE has been shown to be a valuable tracer for sensitive imaging of somatostatin-receptor expression in neuroendocrine tumors and meningioma delineation [115,116]. SPECT resembles PET in its application of radioactive tracers and the detection of gamma rays for image acquisition. However, in SPECT the gamma radiation emitted by the tracer is directly measured, whereas in PET positrons emitted by the applied tracers annihilate with surrounding electrons, causing two gamma photons to be emitted in 180° directions. PET scanners detect photon emissions coincident in time, thereby providing more spatial information of the observed radiation event and, thus, higher image resolution. Different radiotracers can be applied in SPECT for functional imaging of the brain (99mTc-(HMPAO) hexamethylpropylene amine oxime), the myocardium (99mTc-tetrofosmin, 99mTc-sestamibi), malignant (123I- (MIBG) metaiodobenzylguanidine), or inflammatory processes (99mTc or 111In- in vivo labeled leukocytes). However, both functional molecular imaging techniques provide only limited spatial resolution and require complementary morphologic imaging for anatomic mapping and morphologic correlation.

In morphologic imaging, particularly tomographic modalities such as CT and MRI underwent tremendous innovation during the last 15 years currently providing excellent spatial resolution, 3D imaging and increasingly also functional information from tissue perfusion and diffusion. To combine morphologic and functional/molecular information in diagnostic decision making, hybrid imaging with PET/CT has entered clinical routine in oncologic imaging using mostly 18 F-fluorodeoxyglucose (FDG) for cancer

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**Table 1 Novel PET tracers for research and patient care beyond 18 F-fluor-deoxyglucose (18 F-FDG) aim at molecular targets such as integrins and somatostatin receptors or a sensitive for up-regulated amino acid turnover or cell membrane synthesis of tumor cells**

| Nuclide | Tracer | Metabolism | Comment |
|---------|--------|------------|---------|
| 11C     | C - Methionine | Amino acid | Increased amino acid uptake and turnover of tumor cells |
| 12C     | C - Tyrosine | Amino acid |
| 13C     | C - Leucine | Amino acid |
| 18 F    | F - Fluorouracile | Amino acid |
| 18 F    | F - Fluorethytyrosine (18 F - FET) | Amino acid derivative |
| 18 F    | F - Fluorodesoxyglucose (18 F - FDG) | Glucose metabolism |
| 18 F    | F - Fluorazomyzinabinoside (18 F – FAZA) | Hypoxia |
| 18 F    | F - Fluoromisonidazole (18 F – FMISO) | Hypoxia |
| 18 F    | F – Fluthymidine | Proliferation |
| 18 F    | F – Galacto-RGD | p/β3-Integrins |
| 18 F    | F - Arg-Gly-Asp (RGD) Peptide | |
| 18 F    | F - Choline | Prostate carcinoma |
| 18 F    | F - Fluoride | Bone metabolism |
| 68Ga    | 68Ga-DOTATOC/DOTATATE | Somatostatin receptors (SSR) | SSR-overexpressing tumors |

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diagnosis, as predictive imaging biomarker [117], for monitoring of therapy response and radiotherapy planning [118–120]. As a highly sensitive imaging modality based on molecular biology, PET has the ability to assess functional and molecular processes in benign and malignant tissues, which are altered in the earliest stages of virtually all diseases, before morphological changes occur. It compares normal and abnormal tissues on a functional rather than morphological level as MRI and CT. Functional and molecular imaging techniques such as $^{18}$F-FDG-PET/CT can be applied to define a metabolically active biological tumor volume (BTV) for radiation therapy planning [121,122], still limited by its lack of spatial resolution and relatively low specificity to reliably delineate the tumor as accurately as required by precision RT techniques like intensity-modulated radiotherapy (IMRT). $^{18}$F-FDG-PET/CT has the potential to safely decrease radiotherapy volumes by better delineation of tumor and better lymph node detection [123,124] and may be used as predictive/prognostic marker [125,126]. It enables radiation dose escalation [127], and experimentally permits the definition of regions in heterogeneous tumor at greatest risk of recurrence, thus facilitating the redistribution of radiation doses within the tumor to focus on these regions – a principle which is called dose-painting by contours (DPBC) [128]. Another method of specific dose escalation in a PET-positive area is dose painting by numbers (DPBN), where an inhomogeneous radiation dose distribution is intended on a voxel-by-voxel base [129]. Recent developments in PET reconstruction focusing on time-of-flight (TOF) and point spread function (PSF) modeling bear the potential for further improvements in diagnostic performance, as shown by Schaefferkoetter and colleagues [130]. They investigated four different reconstruction schemes on real tumor patient images and found that the application of TOF and PSF modeling may help to optimize particularly the detection of small, low-intensity, focal disease in larger patients.

However, FDG is not a tumor-specific tracer and accumulation in benign lesions, such as regions of inflammation, causes false-positive results with consecutively low specificity [131]. Therefore, novel alternative tracers with higher specificity are under investigation (Table 1), including radiolabeled amino acids for monitoring protein synthesis and radiolabeled choline for monitoring cell membrane synthesis, which may allow for a dedicated characterization of the tumor microenvironment on a molecular level prior to as well as during RT and especially useful in radiotherapy planning, e.g. in high-risk prostate cancer [132]. The amino acid methionine has been used for grading, prognostication and tumor extent delineation for RT planning and showed promising results in the detection and delineation of viable tumors particularly in low-grade gliomas [133]. In clinical practice however, $^{18}$F-labeled PET molecules have revealed advantages compared to those that are $^{11}$C-labeled due to a longer physical half-life of 110 min vs. 20 min. In this regard, $^{18}$F-labeled O–(2) fluoroethyl-L-tyrosine ([$^{18}$F]-PET) is one of the most widely used amino acid tracers [134]. Available data suggests that for RT planning the additional use of [$^{18}$F]-PET-PET to conventional imaging might improve gross tumor volume delineation [135,136]. For PET-based imaging of tumor hypoxia, tracers such as $^{18}$F-fluoromisonidazole ($^{18}$F-FMISO) and $^{124}$I-iodoazomycin galactopyranoside ($^{124}$I-IAZG) were investigated by Riedl and colleagues in rats bearing liver tumors with peritoneal metastasis by dynamic microPET imaging. The authors demonstrated that $^{18}$F-FMISO and $^{124}$I-IAZG localized the same tumor regions to be hypoxic, however with superior diagnostic quality of $^{18}$F-FMISO images in the investigated Morris hepatoma model due to higher count statistics of $^{18}$F-FMISO. Clinically, Thorwarth and colleagues investigated reoxygenation dynamics and its relationship to local control after radiotherapy in a small group of head-and-neck cancer patients ($n = 10$), based on repeated dynamic $^{18}$F-FMISO PET examinations. The authors reported that a tumor control probability model was developed based on repeated $^{18}$F-FMISO PET scans during RT to estimate reoxygenation time which may be applicable for hypoxia image-guided dose escalation in RT [137].

Recently, first hybrid MRI/PET scanners have been installed for patient care combining the excellent soft tissue contrast of MRI with the options of PET in functional and molecular imaging. Compared to CT, MRI provides superior soft tissue contrast together with options for perfusion, diffusion and spectroscopic imaging, as complementing functional parameters, without the use of ionizing radiation [50,138]. The combination of both imaging modalities therefore provides strong synergies for imaging physiological and pathophysiological processes in vivo following multiparametric morphological, functional and molecular imaging concepts in oncology, neurology and cardiology.

Accurate delineation of gross tumor volume is a prerequisite for a successful treatment of cancer with radiotherapy. FDG-PET plays an increasingly important role in radiotherapy that goes beyond staging and selection of patients. For some tumors, such as NSCLC, FDG-PET has led to the safe decrease of radiotherapy volumes, enabling radiation dose escalation and redistribution of radiation doses within the tumor (tumor heterogeneity), along with a significant role in monitoring radiotherapy response. In esophageal cancer and bronchial cancer, FDG-PET/CT has gained significant predictive importance in multimodal treatment settings particularly before, during and after neo-adjuvant radiochemotherapy and is very helpful in target volume
delineation [139,140]. Currently, besides for staging/re-staging purposes, PET/CT is playing a complementary role to other modalities such as CT and MRI for target volume delineation in radiotherapy. Standardized protocols should be established to better define what role PET and/or PET/CT scans should play in radiotherapy planning.

Conclusions

Advances in the understanding of the pathophysiology of cancer have triggered profound developments in multimodality treatment concepts comprising surgery, radiotherapy and molecularly targeted anti-cancer agents. These novel concepts of personalized cancer therapy require careful pre-treatment stratification and timely and efficient therapy monitoring to maximize patient benefit on an individual basis. Therefore, different functional and molecular imaging methods with corresponding biomarkers are currently being developed and characterized pre-clinically with the perspective of clinical translation. Molecularly tailored adaption of MRI, CT, ultrasound, PET/CT (~MRI) and optical imaging modalities represent promising approaches for the demands of targeted combination therapy in radiotherapy oncology.

Competing interests

The authors declare that they have no competing interests.

Authors’ contributions

CC: review concept, literature research and manuscript drafting, MRI and CT section. PMP: literature research and manuscript drafting ultrasound section. ME: literature research and manuscript drafting, Optical Imaging section. DAC: literature research and manuscript drafting, ultrasound section. CR: literature research and manuscript drafting, PET section. KN: literature research and manuscript drafting, MRI and CT section. KL: review concept, literature research and manuscript drafting. FW: review concept, literature research and manuscript drafting. MFR: review concept and manuscript drafting. MRI and CT section. FW: review concept, literature research and manuscript drafting, PET section. KN: literature section. PMP: literature research and manuscript drafting ultrasound section. CC: review concept, literature research and manuscript drafting, MRI and CT section. FW: review concept, literature research and manuscript drafting, PET section. KL: review concept, literature research and manuscript drafting. All authors read and approved the final manuscript.

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