RESEARCH ARTICLE

Correlation of a new index reflecting the fluctuation of parasympathetic tone and fetal acidosis in an experimental study in a sheep model

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Abstract

The autonomic nervous system plays a leading role in the control of fetal homeostasis. Fetal heart rate variability (HRV) analysis is a reflection of its activity. We developed a new index (the Fetal Stress Index, FSI) reflecting parasympathetic tone. The objective of this study was to evaluate this index as a predictor of fetal acid-base status. This was an experimental study on chronically instrumented fetal lambs (n = 11, surgery at 128 +/- 2 days gestational age, term = 145 days). The model was based on 75% occlusion of the umbilical cord for a maximum of 120 minutes or until an arterial pH <= 7.20 was reached. Hemodynamic, gasometric and FSI parameters were recorded throughout the experimentation. We studied the FSI during the 10 minutes prior to pH samplings and compared values for pH > 7.20 and pH <= 7.20. In order to analyze the FSI evolution during the 10 minutes periods, we analyzed the minimum, maximum and mean values of the FSI (respectively FSI_{min}, FSI_{max} and FSI_{mean}) over the periods. 11 experimentations were performed. During occlusion, the heart rate dropped with an increase in blood pressure (respectively 160(155–182) vs 106(101–120) bpm and 42(41–45) vs 58(55–62) mmHg after occlusion). The FSI_{min} was 38.6 (35.2–43.3) in the group pH > 7.20 and was higher in the group pH less than 7.20 (46.5 (43.3–52.0), p = 0.012). The correlation of FSI_{min} was significant for arterial pH (coefficient of -0.671; p = 0.012) and for base excess (coefficient of -0.632; p = 0.009). The correlations were not significant for the other parameters. In conclusion, our new index seems well correlated with the fetal acid-base status. Other studies must be carried out in a situation close to the physiology of labor by sequential occlusion of the cord.

Introduction

The monitoring of fetal well being during labor is essentially based on fetal heart rate (FHR) analysis [1]. The recording of FHR, even continuously during labor, does not fully assess fetal
oxygenation or neonatal risk [2]. Indeed, this tool is imperfect and subjective with an important inter and intra-operator variability [3], despite the existence of classifications [4]. Second-line examinations to characterize the fetal state can be used, i.e. scalp fetal blood sampling to study the fetal acid-base balance (pH or lactates) or study the fetal ECG (ST segment analysis) [5]. These techniques are nevertheless invasive, subject to technical constraints and also STAN is not widespread in North America. There is therefore an important interest in developing both objective and non-invasive means of evaluating fetal well-being.

One of the possibilities studied to better identify fetuses at risk for acidosis is the analysis of changes in the autonomic nervous system (ANS) in response to hypoxia [6,7]. Indeed, the ANS plays a prominent role in the control of fetal homeostasis [8]. Regulation of heart rate is dependent on the ANS and thus, its variability is a reflection of the sympathetic / parasympathetic balance [9]. Spectral analysis is a well-known method of evaluating HRV and high frequency (HF) range (above 0.15 Hz) are centered on the respiratory frequency and related to parasympathetic modulation only [9].

Several publications have studied variations of spectral analysis in fetal acidosis, with conflicting results and a significant individual inter and intra-variability [7,10,11]. In their paper, Casati and Frash pointed out the limitations of the standard spectral approach and concluded that time domain analysis should be preferred [12]. In another study, Frash et al. demonstrated the time domain measure RMSSD (root mean square of successive differences) ability to detect fetal acidemia [13]. We proposed a new continuous tool for the analysis of HRV, the Fetal Stress Index (FSI), taking both advantages of spectral and time domain analysis. Indeed, the FSI uses a spectral analysis (wavelet transform) to filter the signal in order to keep only high frequency oscillations and then computes this oscillations magnitude in the time domain. Our hypothesis is that, because of its reflecting parasympathetic activity, it makes it possible to detect fetuses at risk of acidosis. In a previous study, we shown that this index had a lower inter-subject variability, and a higher effect size compared to other HRV analysis methods [14].

Thus, the aim of this study was to evaluate this new index as a predictive factor of the fetal acid-base state in an experimental model of fetal hypoxia by partial acute occlusion of the cord in pregnant ewes.

**Material and methods**

**Ethics**

The anesthesia, surgery and experimentation protocols were in line the recommendations of the Ministry of Higher Education and Research and the study was approved by the Animal Experimentation Ethics Committee (CEEA # 2016121312148878).

**Surgical preparation**

Eleven near-term pregnant sheep (128 +/- 2 days gestational age, term = 145 days) underwent surgical procedure. Anesthetics and surgical techniques protocols followed those previously described by our team or in the literature [14–16]. Pregnant Charmoise sheep (INRA, Leuderville, France) were fasted 24 h before surgery. Sheep were placed in supine position, intubated, anesthetized with intravenous injection of xylazine (Sedaxylan®, CEVA Santé Animale, France), and maintained with isoflurane 2% (Aerrane®, Baxter, France). The uterus was exteriorized through a maternal midline laparotomy. After hysterotomy, a 4Fr diameter catheter (Arrow®, USA) was inserted into the fetal femoral artery and vein until the abdominal aorta and the inferior vena cava respectively through femoral approach to record gazometric parameters. Electrocardiogram (ECG) electrodes were placed subcutaneously over the chest to record
the fetal ECG. An inflatable silicone occluder was placed around the umbilical cord of all fetuses as also a Doppler probe to record cardiac flow. This probe was placed at the same distance as possible for each surgery and helped to adapt occlusion through the inflate occluder to obtain in each case a 75% reduction of the umbilical flow. A 5F5-diameter catheter (Arrow®, USA) was placed into the amniotic cavity for measuring baseline pressure (intra-amniotic pressure, IAP). The fetal arterial catheter and intra-amniotic catheter were connected to pressure sensors (Pressure Monitoring Kit®, Baxter) that were connected to a hemodynamic monitor (monitor Merlin, Helwett Packard, Palo Alto, CA, USA). The mean arterial pressure (MAP) was measured from the blood pressure phasic signal and referenced to the intra-amniotic pressure (IAP). All hemodynamic data and ECG were recorded using the Physiotrace™ data acquisition board with a 1000 Hz sampling rate (Physiotrace™, Estaris Monitoring, Lille, France) [17].

**Calculation of the Fetal Stress Index (FSI)**

We previously described the HVR analysis and the algorithm used for the calculation of the FSI [14,18,19]. Briefly, the FSI uses a spectral analysis (wavelet transform) to filter the signal in order to keep only high frequency oscillations and then computes this oscillations magnitude in the time domain. The method consists of detecting each heartbeat from R peak of the ECG signal in order to construct the RR series (time evolution of the time intervals between two heartbeats). The RR series is then isolated in a 64 s moving window, normalized and band pass filtered above 0.15 Hz using a wavelet based numerical filter. The remaining oscillations magnitudes are computed by plotting local minima and maxima. The area between the upper and lower envelopes is divided into four subareas A1, A2, A3 and A4. And the AUCmin is defined as the minimum of the 4 subareas. The instantaneous FSI is then computed as:

$$FSI_{inst} = 100 \times \left( a \times \frac{AUCmin + b}{12.8} \right)$$

where a and b are two constants determined on a 200 patients dataset in order to keep the coherence between the visual aspect and the quantitative measurement of FSI. The FSI is then computed as the average value of $FSI_{inst}$ over the last 3 minutes.

**Experimental procedure**

The experiments were starting only after a 48-hour rest of the sheep. During this period, 0.3mL/10kg de Buprenorphine were daily injected to ensure post op analgesia. Before occlusion, a first 30-minute period (stability period) was recorded to ensure that the animals were healthy and representative of the model (normal blood gases and stable hemodynamic parameters). The occlusion was done to obtain a 75% reduction of umbilical flow (controlled with the umbilical probe) and lasted until measurement of a pH $\leq 7.20$ or a maximum duration of 120 mn. Hemodynamic parameters (heart rate, mean blood pressure, intra-amniotic pressure, flow of the umbilical artery) and blood gazes were recorded every 15 minutes. Ewes were not restrained or sedated during the experimentation. After the experiment or in case of miscarriage or fetal death, the animals were sacrificed by an injection of embutramide (T61®, Intervet, France).

**Statistical analysis**

In order to validate the fetal hypoxia model, we first compared hemodynamic and gazometric parameters between periods before occlusion and 15, 30 and 45 minutes after occlusion. Comparisons between time periods were performed using the Friedman non-parametric test. Significance threshold was set at $P < 0.05$. 
To homogenize the results, we chose to present the results by pH category. The thresholds of 7.20 was retained in accordance with those already used in the literature and the clinical implication of such a pH when performing a fetal blood sample [20]. The data of the different parameters during occlusion were compared between pH > 7.20 and pH ≤ 7.20. The importance of the early detection of fetal hypoxia being able to intervene before the occurrence of asphyxia, and thus avoid possible neonatal brain sequelae, we chose to study the FSI evolution during the 10 minutes prior to pH samplings. We therefore analyzed the minimum, maximum and mean values of the FSI (respectively FSI_{min}, FSI_{max} and FSI_{mean}) over these periods.

Hemodynamic, gazometric parameters and the FSI_{min}, FSI_{max} and FSI_{mean} were expressed as median and interquartile range (1^{st} quartile-3rd quartile). Comparisons between pH > 7.20 and pH ≤ 7.20 were performed using the Wilcoxon non-parametric test. Significance threshold was set at P < 0.05. The relationships between gazometric parameters (pH, pO2, pCO2, lactates and base deficit) and FSI values were evaluated using the Spearman Rho correlation coefficients. The software used was SPSS 20.0 (IBM, Armonk, NY, USA).

Results

11 experimental procedures were performed and 3 were excluded for unusable datas (rapid fall of pH in 2 cases, no gazometric datas in one case due to a thrombus the arterial catheter). No miscarriage or fetal death occurred. Table 1 shows the gazometric and hemodynamic datas time evolution. Before occlusion, ewes were healthy with a normal (pH = 7.40). At T = 15mn, we observed a bradychardia (106 bpm vs 160 before occlusion) and an hypertension (58 vs. 42 mmHg). Gazometric parameters showed a median pH of 7.23 with an hypoxemia (pO2 = 11.5mmHg) and a rise of lactates, pCO2 and base deficit. All pH were superior to 7.20. At T = 30mn, hemodynamic parameters were stable. In 6 experimentations, pH was less than 7.20. At T = 45mn, median pH was 7.12 and all were inferior to 7.20. We observed metabolic acidosis with lactates at 5.83 mmol/l and base deficit at 11 mmol/l.

Table 2 shows hemodynamic, gazometric and FSI variations according to the pH ranges during occlusion. Lactates were significantly higher for pH > 7.20 (p = 0.012) whereas other gazometric parameters didn’t vary significantly. Heart rate and arterial pressure remained the same between pH > 7.20 and pH ≤ 7.20.

The FSI_{min} was 38.6 (35.2–43.3) for pH > 7.20 and was higher for pH ≤ 7.20 (46.5 (43.3–52.0), p = 0.012) (Fig 1). FSI_{max} and FSI_{mean} didn’t show significant variations between pH > 7.20 and pH ≤ 7.20 (Table 2). The correlation between FSI_{min} and hemodynamic—gazometric parameters is shown in Table 3. The correlation was significant for arterial pH

| Table 1. Physiological fetal datas in time series (n = 8). |
|-----------------|-----------------|-----------------|-----------------|-----------------|
|                 | Before occlusion| After occlusion | After occlusion |
| Heart rate (bpm) | 160(155–182)    | 106(101–120)*   | 103(94–122)*    | 99(89–127)*     | 0.002 |
| Art pressure (mmHg)| 42(41–45)      | 58(55–62)*       | 57(54–59)*       | 59(55–65)*       | 0.002 |
| pH              | 7.4(7.4–7.4)   | 7.23(7.22–7.25)* | 7.18(7.11–7.20)* | 7.12(7.08–7.14)* | <0.0001 |
| pO2 (mmHg)      | 16(15–18.25)   | 11.5(10.25–12.75)* | 13(11.25–13.75)* | 13(12–14)*       | 0.002 |
| pCO2 (mmHg)     | 36.1(29.7–39.7)| 48.1(40.2–57.9)* | 53.7(41.3–64.5)* | 59.4(55.9–64.9)* | 0.002 |
| Lactates (mmol/l) | 0.89(0.76–1.38)| 2.57(1.94–3.62)* | 4.47(3.06–5.40)* | 5.83(5.04–6.61)* | <0.0001 |
| Base deficit (mmol/l) | 3.5(0–6.75)  | 6.5(2.25–9.75)*   | 7.5(4–13.75)*    | 11(9–11)*        | 0.026 |

Results presented as median and interquartile. p values represent the comparison between the four periods (Friedman test).

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Table 2. FSI variation according to pH ranges during occlusion.

|                         | pH > 7.20 | pH ≤ 7.20 | p     |
|-------------------------|-----------|-----------|-------|
| Heart rate (bpm)        | 106(101–120) | 106(97–129) | 0.499 |
| Arterial pressure (mmHg)| 57.5(55.25–62.25) | 57(55.5–64.25) | 1.000 |
| pH                      | 7.23(7.22–7.27) | 7.17(7.14–7.18) | 0.012 |
| pO₂ (mmHg)              | 11.5(10.25–12.75) | 13(11.25–13.75) | 0.356 |
| pCO₂ (mmHg)             | 48.1(40.2–57.9) | 50.8(38.9–63.6) | 1.000 |
| Lactates (mmol/l)       | 2.57(1.94–3.62) | 4.47(2.92–5.57) | 0.012 |
| Base deficit (mmol/l)   | 6.5(2.25–9.75) | 9.5(6.25–14.5) | 0.058 |
| FSI_{min}               | 38.6(35.2–43.3) | 46.5(43.3–52) | 0.012 |
| FSI_{max}               | 64.6(61.4–74.9) | 67.7(58.7–73.2) | 0.779 |
| FSI_{mean}              | 52.1(47.8–59.4) | 56.4(51.9–63.2) | 0.123 |

Results presented as median and interquartile. p values represent the comparison between the two groups (Wilcoxon test).

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Fig 1. Fetal Stress Index according to pH. FSI_{min} according to pH during occlusion (n = 8). The data are presented as median ± interquartile. *: p<0.05 versus pH > 7.20.

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For the 2 cases excluded due to rapid fall of pH, fetal sheep were hypoxemic before occlusion with baseline $pO_2$ values lower than 15 mmHg.

**Discussion**

The aim of fetal monitoring during labor is to detect fetuses at risk of developing respiratory and metabolic acidosis, which could result in brain lesions or even perpartum death [21,22]. This monitoring is based primarily on the continuous recording of the FHR, which does not, however, allow a perfect evaluation of oxygenation of the fetus and whose limits of interpretation are well known. The current second-line examinations are invasive and are only feasible under certain conditions, with controversial efficacy [23,24]. The objective of this experimental study on fetal lamb was to evaluate a new index based on the analysis of the parasympathetic ANS activity through HRV. Our results showed a good correlation between pH and FSI and that this index made it possible to predict the occurrence of moderate acidosis.

In order to obtain acidosis, we chose a model of chronically instrumented fetal lambs with occlusion of the umbilical cord. Several experimental models of fetal hypoxia are found in the literature, particularly in fetal lamb: partial occlusion of the maternal aorta, occlusion of uterine or hypogastric arteries, repeated umbilical cord total occlusions of varying duration and frequency, or maternal hypoxemia by oxygen depletion of the air inspired by the mother [25,26]. In our study, we chose to achieve partial, acute and prolonged occlusion of the umbilical artery (reduction of 75% of the flow) in order to obtain a gradual decrease of the pH allowing the analysis of the phenomena of fetal adaptation brought into play. Indeed, occlusion was responsible for a fall in heart rate and an increase in mean arterial pressure. Several studies have shown that bradycardia and peripheral vasoconstriction were secondary to activation of the carotid receptor block after sinocarotidial and sinoaortic denervation [27,28]. Indeed, the reduction in the size of the common umbilical artery during occlusion is mechanically

| Gazometric parameter | AP      | HR      | pH     | $pO_2$  | $pCO_2$ | Lact. | BD      |
|----------------------|---------|---------|--------|---------|---------|-------|---------|
| Correlation coefficient (r values) | 0.368   | 0.0049  | -0.671 | 0.142   | 0.311   | 0.024 | 0.63    |
| $p$                  | 0.161   | 0.858   | 0.004  | 0.60    | 0.24    | 0.0931| 0.009   |

HR: Heart rate; AP: Arterial pressure; Lact.: Lactates; BD: Base deficit

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Fig 2. Correlation curve between FSI$_{min}$ and arterial pH.

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The increase stimulates baroreceptors in the carotid sinus and aorta, resulting in a vagus-mediated parasympathetic response that decreases heart rate [30]. However, the role of baroreflex is discussed by some teams [8]. Indeed formal studies on sheep confirm that the baroreflexes are immature before birth [8,31]. Thus, modern interpretation is that the baroreflex makes only a limited contribution to fetal adaptation to asphyxia and the main actor is the chemoreflex.

We carried out an original analysis of the HRV based both on spectral and time analysis. Indeed, the FSI uses a spectral analysis to filter the signal in order to keep only high frequency oscillations and then computes these oscillations magnitudes in the time domain. At present, there is no standardized method for analyzing fetal HRV and different techniques have been proposed: time analysis with the RR interval study or spectrum analysis of heart rate fluctuation frequencies using the Fourier or Wavelet transform [6,13,32,33]. In the literature, some studies have separated in high from low frequencies spectral content, while others studied the total spectral band [6,7,10]. Thus, there is as yet neither method currently used in routine of HRV analysis nor any clinical reference analysis.

In our experimental study with continuous acute occlusion of the cord and outside the labor period, we observed an increase in our index as soon as moderate acidosis occurred (from 7.20). The study of the correlations showed that our index was correlated to the variation of the pH and with the base deficit. Other studies have investigated changes in HRV by spectral analysis in acidosis situations [6,7,10]. These studies collected the ECG signal from a fetal scalp electrode and proposed an a posteriori comparison of HRV, either with respect to scalp pH or with cord pH at birth. Siira, et al. carried out the analysis of the correlation between HRV and the pH value during labor (scalp pH) on 543 fetuses [6]. They found an increase in total HRV in the fetus group with scalp pH <7.20 (81 fetuses) compared to those with a pH ≥7.20 (462 fetuses). However, in the subgroup of fetuses with a pH <7.10, HRV was similar to that of normoxic fetuses. Furthermore, Van Laar, et al. found no correlation between HRV in high or low frequencies in the human fetus during labor for scalp pHs between 7.20 and 7.25 in case of absolutes HRV parameters (study on 39 pH in utero in 30 patients, signal collected by scalp electrode) [34]. However, after normalizing the values (division of LF and HF power by the total power), they found an increase in the normalized HF and a decrease in normalized LF when the intrauterine pH decreased. In another study analyzing a posteriori RCF recordings 1 h before the birth of neonates with severe acidosis compared to neonates with a pH >7.20, Van Laar, et al. reported an increase LF and a decrease HF within 30 minutes before birth in the newborn group with a pH <7.05 compared to the others [7]. In a first pilot retrospective
study, we also found a decrease of our index in case of pH less than 7.15 during second stage of labor [19].

Thus, divergent results are found on the variations of HRV according to the studies, probably due to techniques (measurement of the total HRV, normalization of the LF and the HF...) but also of different measurement conditions (scalp sample or neonatal pH). Our index appears promising because of its ease of interpretation (numerical data), its continuous character and its ability to detect situations of moderate hypoxia. It could therefore be a warning sign for acidosis.

However, this experimental study has several limitations. The first one is that of being an animal model. Indeed, despite many similarities between sheep and human gestation, the reproducibility of our physiopathological observations and therefore the extrapolation to the human fetus must therefore be considered with caution. Our model can be also discussed. It is not like a labor insult, neither a clinical scenario, but we aim to evaluate the variation in case of acute hypoxia as proposed by many other authors [35–37]. It would be interesting to modify our model to approximate the physiology of labor through sequential occlusions that recall the effect of uterine contractions as described by several authors [22,38,39]. It will be also interesting to evaluate the use of nitrogen to lower maternal and thus fetal pO2 in a controlled manner without effecting fetal perfusion. At last, we observed only 48h of rest after surgery and fetal pO2 at the start of the experiments was low and possibly reflected the effects of the surgical procedure. It could be considered moderately hypoxic and it will be important in future projects to ensure a longer period of recovery.

Conclusion

In this experimental study, our new index seems well correlated with the fetal acid-base status. Other studies must be carried out in a situation close to the physiology of labor by sequential occlusion of the cord.

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