Impact of nonsurgical spinal decompression on paraspinal muscle morphology and mechanical properties in young adults with low back pain

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Abstract
Objective: The mechanism underlying the benefit of nonsurgical spinal decompression (NSSD) on low back pain is unclear. This study was performed to investigate the immediate impact of NSSD on the mechanical properties and morphology of the paraspinal muscles.

Methods: Participants with low back pain were recruited. NSSD therapy was provided on one occasion. A myotonometer was placed perpendicularly on the skin surface over the paraspinal muscle at the level of L₃/L₄ to measure the mechanical muscle properties. The multifidus thickness was measured using B-mode ultrasound and defined as the distance between the transverse process and subcutaneous tissue fascia. The difference between before and after NSSD was analyzed by a paired t-test.

Results: Thirty participants (mean age, 20.9 ± 0.8 years; 9 male, 21 female) were recruited. No significant difference was observed in the muscle mechanical properties or morphology between before and after the intervention.

Conclusions: NSSD intervention did not induce immediate changes in the paraspinal muscle mechanical properties or multifidus thickness in young adults with low back pain. NSSD might produce benefits by stimulating mechanical receptors rather than inducing morphological changes.
or mechanical property alterations of the muscle fibers. These parameters may not be suitable outcome measures for NSSD intervention.

**Keywords**
Nonsurgical spinal decompression, paraspinal muscle, morphology, mechanical properties, low back pain, myotonometry

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**Introduction**

A report published by the World Health Organization indicated that chronic low back pain (LBP) is among the most common causes of long-term disability.\(^1\) The prevalence of LBP among young adults is reportedly 42.4% and continues to rise.\(^2\) Studies published from different countries have shown that 30% to 81% of university students experience recurrent chronic LBP\(^3\)\(^,\)\(^4\) that interferes with social, physical, and academic activities.\(^5\) The incidence of LBP among young adults has long been underestimated, and limited clinical data from this age group have been recorded.

The multifidus and transversus abdominis are the primary spinal stabilization muscles, and a considerable amount of work has been conducted to understand their role in LBP.\(^6\) The two muscles have different roles in maintaining lumbar stability because of their anatomical structure and functional coupling.\(^7\) The transversus abdominis maintains spinal stability by contraction, which increases the abdominal pressure.\(^8\) Dysfunction of the transversus abdominis in nonspecific LBP is related to motor control (i.e., delayed activation relative to the multifidus during functional movement).\(^9\)\(^,\)\(^10\) The tension load of the common tendon of the transversus abdominis is primarily transferred to the posterior thoracolumbar fascia to maintain the stability of the spinal column. The multifidus directly maintains lumbar stability through the thoracolumbar fascia, which provides more than two-thirds of the spinal stability.\(^11\)\(^,\)\(^12\) An ultrasound imaging study revealed a smaller percent thickness contraction of the multifidus in people with than without chronic LBP.\(^13\) Animal experiments have shown that a prolonged static position\(^14\) and repetitive stress contribute to spasm of the multifidus.\(^15\) In addition, the pain level was demonstrated to be associated with the ability to recruit the multifidus.\(^16\)

Muscle spasm refers to sustained contraction of a muscle,\(^17\) and the increase in chronic tension contributes to pain.\(^18\) Muscle tone can be defined as the resting tension of the muscle or the resistance in response to stretching of the muscle.\(^19\) Altered lumbar muscle tone was found in adults with chronic LBP\(^20\)\(^,\)\(^21\) and was suggested to be associated with the underlying pathologies and symptoms.\(^22\) Early literature indicated that muscle tone is a contributing factor to the pain-spasm-pain model.\(^23\) A vicious circle is established in which pain results in increased muscle tone, which in turn causes further pain.\(^24\) Pain adaptation models postulate that pain itself reduces activation of muscles, thus reducing the range of motion and movement velocity.\(^25\) This in turn leads to inappropriate body positioning at rest and during motion. Stiffness can be interpreted
as the viscoelastic property of muscles. A muscle that has high static stiffness requires more energy to activate and is therefore more difficult to contract. Studies that used shear wave elastography confirmed increased stiffness of the paraspinal muscles in people with chronic LBP.

Nonsurgical spinal decompression (NSSD) is a technique that applies longitudinal traction force through the muscle to distract the spinal column via a mechanical or motorized pulley system. The stretching force is reportedly able to reduce muscle tension by elongating the muscle fibers and widening the intervertebral foramen. The available evidence regarding traction in the management of LBP is controversial. Several systematic reviews showed no beneficial effect of traction intervention when compared with placebo in terms of pain relief and returning to work but repeatedly indicated that more high-quality studies are required. Despite the apparent lack of evidence to support the use of lumbar traction in the management of LBP, traction continues to be a commonly used intervention by health care professionals to distract tissues and joints in the lumbar spine region. A survey published in 2005 indicated that 41% of the surveyed physiotherapists used lumbar traction in the management LBP. Similar survey data were collected from a group of physiotherapists in 2015. The results indicated that 76.6% of the respondents used lumbar traction in the management of LBP. The divergence between clinical practice and recommendations from systematic reviews may be related to the empirical evidence that supports the benefits of lumbar traction. These studies indicated the potential efficacy of NSSD in patients with LBP.

One proposed mechanism of NSSD is a reduction of muscle spasm, which inhibits nociceptive impulses and increases mobility. However, the impact of NSSD on muscle morphology and the mechanical properties of tone and stiffness have been less intensively studied. Thus, it may be possible to assess the impact of NSSD from the perspective of mechanical muscle properties. Early studies attempted to quantify altered muscle tone in people with chronic LBP using surface electromyography (EMG). The possibility of using surface EMG as an outcome measure of NSSD has been reported in some studies; however, the results of these studies were rather inconclusive because of conflicting evidence. The limitation of using the electrical activity level as a surrogate for muscle tone is that the electrical activity mostly concerns the muscle contraction elicited by the neural electrical drive of motor nerves and muscle cells, not the endogenous contractile structures of skeletal muscles. In addition, little is currently known on the immediate impact of NSSD on paraspinal muscle morphology and whether it is possible to assess changes in muscle tone using a myotonometer in young people with chronic LBP. Thus, an understanding of how the mechanical properties of muscles are affected by NSSD would improve our understanding of the intervention technique that would facilitate treatment selection. This study was performed to assess the immediate impact of NSSD of the multifidus thickness and paraspinal muscle mechanical properties.

**Methods**

**Participants**

Participants were recruited from the student and staff populations of a local institute via social media and internal announcements. The inclusion criteria were an age of 18 to 25 years, the presence of chronic nonspecific LBP (in the lumbar and lumbosacral regions) for >3 months prior to enrollment,
and no treatment for ≥4 weeks prior to enrollment. The exclusion criteria were a body mass index of >30 kg/m², a history of fracture or surgery in the low back area, pregnancy, a herniated disc, lumbar instability, and malignancy. A physical therapist diagnosed LBP based on the clinical assessment protocol established by the American College of Physicians and American Pain Society. Demographic information regarding age, sex, height, weight, and clinical history of LBP were collected at the beginning of the data collection session. Clinical information regarding back pain was also collected. The Chinese version of the Oswestry Low Back Pain Disability Index was used to assess the degree of disability related to back pain. The Japanese Orthopedic Association back pain score was recorded to assess the disorder in different dimensions, including quality of life, pain intensity, and degree of disability. A numerical pain rating scale was used to assess the pain intensity (range, 0–10) that the participants were experiencing at the time of data collection.

**Sampling method and sample size**

This study adopted a pragmatic sampling method. Participants who met the inclusion criteria were recruited into the study. The sample size calculation was based on a pilot trial involving six participants. Muscle tone was used as the primary outcome measure for the sample size calculation. The sample size was calculated with the software GPower version 3.1.2, using the “A priori: Compute required sample size –given α, power, and effect size” as the type of power analysis. The preliminary results indicated a mean difference of 0.43 Hz (standard deviation, 0.66) after NSSD, which gave an effect size of 0.63. With an α error probability of 0.05 and a power of 0.95, a sample size of 27 was sufficient for the present study.

**Parameters**

The mechanical properties of muscle tone and stiffness at the L3/L4 facet joint level were recorded with a myotonometer (MyotonPRO; Myoton AS, Tallinn, Estonia). The oscillation frequency (Hz) indicates the tone (i.e., intrinsic tension) of a muscle in the resting state. The dynamic stiffness (N/m) characterizes the resistance of the muscle to contraction. The morphology parameter of multifidus thickness (mm) at the L3/L4 facet joint level was assessed by diagnostic ultrasound (M-Turbo; FUJIFILM SonoSite, Inc., Bothell, WA, USA).

**Ethics**

The study protocol was approved by the Medical Ethics Committee of the First Affiliated Hospital of Sun Yat-sen University [approval no.: 2016(85)]. All participants were informed of the study procedure and the right to withdraw from the trial at any time. Written consent was obtained from all participants.

**Study procedure**

**Myotonometry**

The muscle tone and stiffness of the lumbar paraspinal muscles were assessed by a handheld myotonometer before and after the NSSD intervention. The validity and reliability of using a myotonometer to measure muscle tone and stiffness was published in previous studies. The intraclass correlation coefficient for test–retest reliability within the same day was reported to be 0.99 for bilateral muscle tone and stiffness. The standard error measurement for muscle tone was 0.06 Hz on the left and 0.03 Hz on the right.
For muscle stiffness, the standard error measurement was 1.82 Hz on the left and 2.15 Hz on the right. The participants were asked to lie in the prone position on the traction table with their hands on both sides of their head, exposing the lumbar region. The test site was determined by palpation. The examiner located the L₄/L₅ interspinous space by palpating the highest level of the iliac crest, and then located the interspinous space of L₃/L₄. The test sites were marked on the skin surface 1 cm lateral to the left and right spinous processes. The myotonometer was set to triple scan mode in which three consecutive indentations were applied (0.4 N, 15 ms apart). The probe was placed vertically at the location markers to record the muscle tone and stiffness of the bilateral L₃/L₄ paraspinal muscles.

**Ultrasound imaging**

An experienced examiner obtained all images using a portable ultrasound machine with a 5.0-MHz convex array probe before and after the intervention. The participants lay in the prone position on the traction table with their hands on both sides of their head, exposing the lumbar region. The scanning procedure was based on a published protocol. The examiner first identified the spinous process of L₄ and placed the probe longitudinally along the spine with the midpoint over the L₄ spinous process. The probe was then moved laterally and angled slightly medially until the L₃/L₄ facet joint could be identified. The scan point was directly over the multifidus, and a measurement from this landmark was taken to record the linear distance between the transverse process and the inner layer of the lumbodorsal fascia. The measurement of the multifidus thickness is illustrated in Figure 1.

The contralateral arm-lifting task was conducted to contract the multifidus. The participants lay in the prone position and performed isometric contraction with the elbow flexed to 90° and shoulders abducted to 120°. The participants then lifted their head, trunk, and upper extremities and held this position with maximum effort (determined as grade 5 on the manual muscle test) against a load applied at the elbow for 5 seconds.

![Figure 1. Ultrasound image used for measurement of multifidus thickness.](image-url)
**NSSD**

An NSSD system (Model No. SDS9800; Ryzur Medical Technology Company, Beijing, China) was used to apply a continuous decompression force to a specific intervertebral level. Pressure was applied at two levels with the maximum force maintained for 60 seconds and the minimum force maintained for 30 seconds. The maximum decompression force was calculated as half the participant’s body weight (lbs) plus 10 lbs, and the minimum force was calculated as half the participant’s body weight minus 10 lbs. Eighteen cycles were performed within the session. The decompression force was applied for 28 minutes 15 seconds with a traction force angle of 20° to target the L3/L4 facet joint. The participants were positioned supine and fixated on the instrument bed by straps located at the chest and pelvic levels. The hip and knee joints were flexed to 30° and 60°, respectively, by placing an inflatable pad under the knees for relaxation and maintenance of the lumbar physiological curve. The NSSD protocol was conducted in accordance with the manufacturer’s operation manual.47

**Statistical analysis**

Data were analyzed using the software SPSS version 20.0 (IBM Corp., Armonk, NY, USA). The demographic and clinical baseline characteristics were summarized by descriptive statistics. The differences in the multifidus thickness and paraspinal muscle mechanical properties between before and after the intervention were assessed by the paired t-test. A p value of <0.05 was considered statistically significant.

**Results**

**Demographics**

Thirty participants with chronic LBP took part in the study (mean age, 20.9 ± 0.8 years). Table 1 presents a summary of the demographic information of the sample population. The clinical information of LBP of the sample population is presented in Table 2.

**Multifidus thickness**

The paired t-test indicated no significant difference in the multifidus thickness either at rest or during contraction between before and after NSSD at the L3/L4 level. Table 3 shows the measurements of the multifidus muscle thickness.

**Muscle tone and stiffness of paraspinal muscles**

The changes in the paraspinal muscle tone and stiffness after NSSD were not...
Table 3. Multifidus thickness at rest and in contracted state before and after NSSD intervention.

| Thickness, mm | Minimum | Maximum | Mean | SD | diff | p value |
|---------------|---------|---------|------|----|------|---------|
| Relaxed state |         |         |      |    |      |         |
| Left Pre      | 8.95    | 30.86   | 20.62| 4.13|      |         |
| Post          | 10.15   | 27.81   | 20.48| 3.80| 0.15 | 0.72    |
| Right Pre     | 11.79   | 34.13   | 21.55| 4.49|      |         |
| Post          | 12.79   | 32.48   | 21.13| 4.56| 0.43 | 0.21    |
| Contracted state |      |         |      |    |      |         |
| Left Pre      | 16.45   | 40.81   | 28.48| 4.46|      |         |
| Post          | 16.46   | 40.19   | 28.61| 4.87| −0.13| 0.78   |
| Right Pre     | 15.64   | 44.46   | 29.66| 5.21|      |         |
| Post          | 16.49   | 44.08   | 30.06| 5.24| −0.40| 0.45   |

NSSD, nonsurgical spinal decompression; SD, standard deviation; Pre, before NSSD; Post, after NSSD; diff, difference.

Table 4. Mechanical muscle properties before and after NSSD intervention.

| Mechanical properties | Minimum | Maximum | Mean | SD | diff | p value |
|-----------------------|---------|---------|------|----|------|---------|
| Tone, Hz              |         |         |      |    |      |         |
| Left Pre              | 11.0    | 18.9    | 15.04| 1.77| −0.03| 0.78   |
| Post                  | 11.3    | 19.9    | 15.07| 1.71|      |         |
| Right Pre             | 11.7    | 19.8    | 15.36| 1.88| −0.08| 0.41   |
| Post                  | 12.1    | 20.9    | 15.44| 1.86|      |         |
| Stiffness, N/m        |         |         |      |    |      |         |
| Left Pre              | 128     | 450     | 267.77| 67.06|     |         |
| Post                  | 131     | 432     | 269.67| 63.87| −1.90| 0.72   |
| Right Pre             | 152     | 444     | 281.53| 74.89| −1.37| 0.75   |
| Post                  | 161     | 487     | 282.90| 73.50|      |         |

NSSD, nonsurgical spinal decompression; SD, standard deviation; Pre, before NSSD; Post, after NSSD; diff, difference.

Discussion

This study is among the first to investigate the impact of NSSD on the paraspinal muscle morphology and mechanical properties in young adults with LBP by ultrasonography and myotonometry. The results indicated no significant differences in the multifidus thickness, tone, or stiffness of the paraspinal muscles immediately after NSSD.

Multifidus thickness

This study investigated the immediate morphological changes in the multifidus after NSSD intervention. Elongation of muscle fibers is believed to play a role in pain relief by stimulating the mechanical receptors located at the paraspinal ligaments and muscles.33 One published study revealed thinning of the psoas major during mechanical traction.48 Other studies that investigated the effect of stretching on peripheral muscle thickness also showed a reduction of muscle thickness after the stretching intervention.49 The finding of the present study is consistent with a study that used ultrasonography to study the thickness of the trapezius and splenius capitis.50 That study showed a reduction in muscle thickness during mechanical traction, but the difference did not reach statistical significance.50 However, the results of that study and the present study may not be directly comparable because of the differences in the statistically significant. Table 4 shows the measurements of the paraspinal muscle tone and stiffness.
muscles tested and amount of force applied. A potential reason for the lack of significant changes observed in this study is the short intervention period, which was not sufficient to induce morphological change. A systematic review indicated that structural muscle changes tended to occur in stretching programs that lasted for >8 weeks. The stretching duration of 28 minutes in this study may therefore be insufficient to induce morphological changes. The lack of a significant difference in the multifidus thickness may add further support to the theory that the benefits of NSSD are associated with stimulation of mechanical receptors. The potential pain-relieving mechanism of NSSD may be similar to that of spinal manual therapy, such as spinal manipulation, in terms of decreasing the sensitivity within the muscle spindles and increasing the pressure pain threshold.

**Mechanical muscle properties**

Spasm of the paraspinal muscles is believed to be a contributing factor to chronic LBP. Some published studies investigated paraspinal muscle activity by EMG during different lumbar traction protocols of varying distraction-force waveforms and pull angles. These studies showed no significant differences in the EMG signal of the lumbar erector spinae between any of the traction groups and the control group. One study that assessed the effects of cervical traction on muscle activity also showed that the EMG activities of the lateral neck muscles did not differ significantly immediately after intermittent mechanical traction. These results suggest that traction may not have an immediate impact on muscle tone. The present study did not reveal a significant decrease in muscle tone. The difference in muscle tone after the intervention also did not reach the minimal detectable difference previously reported for this pathology group. This finding is consistent with the EMG study showing that NSSD is unlikely to affect muscle tone after one session and casts doubt on the suitability of using muscle tone as an outcome measure after each treatment session, either by myotonometry or palpation.

Muscle stiffness refers to the elastic properties of muscle and plays an important role in the stabilizing system of the spine. Abnormal muscle stiffness is considered to be a contributing factor to chronic LBP. Passive stretching of muscle is reportedly able to reduce muscle stiffness by affecting the muscle–tendon complex. Published studies that investigated the effect of stretching on the gastrocnemius showed a reduction in muscle stiffness after 60 seconds of static stretching. The present study did not reveal a significant reduction in paraspinal muscle stiffness after 28 minutes of the NSSD intervention. A possible reason for the lack of significance is that the paraspinal compartment is encapsulated by various layers of connective tissue and myofascia. The stiffness of these tissues may not be affected under physiological conditions or within normal physiological ranges. This theory is supported by a study that investigated the changes in paraspinal muscle stiffness in five postures that aimed to stretch the paraspinal column. Stretching performed in all postures produced no significant changes in the paraspinal muscle stiffness. Another study that used a spinal manipulation technique to alter paraspinal muscle stiffness also showed no significant difference in stiffness after the intervention. These findings add further evidence that the paraspinal muscle stiffness might not be affected by passive stretching alone. Thus, the benefit of NSSD is unlikely to be related to alteration of the muscle stiffness, and stiffness may not be a suitable outcome for the NSSD intervention. These results suggest
that muscle spasm reduction and muscle relaxation are not the mechanisms underlying how NSSD alleviates back pain.63

Limitations
The results of the present study should be interpreted with caution. This study provided only a single dose of treatment and did not assess the impact of NSSD on the muscle mechanical properties and morphology throughout an entire course of intervention. It is therefore difficult to conclude whether NSSD can induce significant changes after performance of more intervention sessions. Additionally, the findings of the present study may not be extrapolated to the general population. However, this is unlikely to affect the validity of the findings because very few reports have indicated that young adults would respond differently to NSSD intervention. Published clinical management guidelines for LBP also do not indicate that young adults would respond differently to intervention. Finally, the present study did not include a control group or comparison with other types of intervention. The NSSD protocol adopted in the present study followed the manufacturer’s recommendation. A systematic review indicated that a large variation was present in the lumbar spine traction protocol within published randomized controlled trials. Parameters such as the force, force angle, and intervention duration appeared to be chosen arbitrarily.64 Thus, there is no definitive evidence to adequately justify the parameters of the NSSD setting.

Conclusions
The findings of the present study indicate that NSSD does not induce immediate changes in the mechanical properties or morphology of the paraspinal muscles after a single dose of treatment in young adults with LBP. This may further support the notion that NSSD produces benefits by stimulating mechanical receptors rather than by inducing morphological changes or mechanical property alterations of muscle fibers. Therefore, these parameters may not be suitable outcome measures for NSSD intervention.

Availability of data and materials
The dataset supporting the conclusions of this article is available from the authors upon request.

Consent to publish
All participants provided consent to publish their individual data.

Declaration of conflicting interest
The authors declare that there is no conflict of interest.

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