Cigarette smoking remains common around the world and is a well-known cause of functional lung impairment, mainly chronic obstructive pulmonary disease (COPD). Currently, COPD is the third cause of death worldwide and responsible for approximately 6% of total deaths (1). Spirometry is required to establish the diagnosis and severity of COPD, but pulmonary function tests (PFT) have some important limitations: technical difficulties in patients with respiratory problems, relative insensitivity at the early stage of disease and the inability to distinguish subtypes of COPD or provide regional information (2,3).

COPD is considered a complex heterogeneous disease in which disease presentation and course can vary greatly between individual patients and over time. Indeed, despite a similar degree of airflow limitation, patients can present with different clinical outcomes such as respiratory symptoms and exacerbations (4). As a consequence, many studies have been performed in order to identify subtypes of COPD, i.e., phenotypes. PFT results alone may not be sufficient to capture these phenotypes, as the amount of emphysema, small airway disease, and bronchial inflammation cannot be distinguished.

Computed tomography (CT) is an established imaging technique that can be used to capture multiple characteristics of COPD in a non-invasive manner (5,6). By using CT, global and regional information can be obtained. A radiologist can perform radiologic characterization visually by qualitatively scoring several characteristics of COPD. A guideline to standardize and visually categorize patterns of emphysema, airway disease, and associated features has been published by the Fleischner society (7). In this statement, emphysema is categorized as centrilobular emphysema (subclassified as trace, mild, moderate, confluent, and advanced destructive), paraseptal emphysema (PSE, subclassified as mild or substantial), or panlobular emphysema. In the absence of emphysema, airway disease can be a dominant feature of COPD and can be expressed as thickening of bronchial walls, micronodular peripheral opacities, or by gas trapping on expiratory CT.

Visual assessment of emphysema has been associated with impaired lung function, higher risk of mortality, genetic loci associated with COPD, and lung cancer (8-12). However, visual analysis is time consuming and subjective. Alternatively, quantitative assessment can be performed. This may be helpful in providing an objective measure for risk stratification and can be used to analyze large datasets of CT scans, for example in lung cancer screening programs (9,13,14). Multiple studies have been performed to evaluate the most paramount CT-features, but up until now, CT quantification techniques are not widely used in clinical setting.

Recently, Kang et al. evaluated the relationship between visually assessed CT subtypes of COPD with quantitative CT characteristics and clinical traits in a recently published study in the Journal of Thoracic Disease (15). They included 452 participants from the Chronic Obstructive Pulmonary Disease in Dusty Areas (CODA) cohort, which includes Korean COPD patients living near cement plants. They visually categorized patients into 7 subtypes: normal, PSE, bronchial airway disease (and absent or trace emphysema or mild PSE), trace centrilobular emphysema, mild centrilobular emphysema, moderate centrilobular emphysema, and confluent and advanced destructive emphysema.
The results of Kang et al. confirmed previously suggested associations: (I) body mass index (BMI) was lower in patients with a higher degree of emphysema and relatively higher in the bronchial airway group; (II) pulmonary function lowered as the degree of emphysema worsened; (III) Pi10 was highest in the bronchial disease subtype; (IV) emphysema and functional small airways disease as assessed by parametric response mapping (PRM<sub>Emph</sub> and PRM<sub>SAD</sub>, respectively) were raised as the visual grade of emphysema worsened; (V) PRM<sub>Emph</sub> increased with severity of emphysema subtypes; (VI) PRM<sub>SAD</sub> was increased in the trace emphysema group as compared to the normal group and decreased slightly in the mild emphysema group.

The PSE subtype was explored in more detail. Participants with PSE had lower lung function and higher PRM<sub>Emph</sub> as compared to participants with moderate centrilobular emphysema. PRM<sub>SAD</sub> was lowest in participants with PSE. PSE was categorized regardless of other imaging characteristics, thus participants in the PSE subcategory could have centrilobular emphysema or bronchial airway thickening as well.

Kang and colleagues force us to take a step back and contemplate the value of automatic quantification. As stated before, many studies have been published on automatic quantification techniques that are able to assess several traits of COPD. But why are pulmonologists and radiologists apprehensive for using it in clinical practice?

Already in 1978, shortly after the introduction of CT, the first quantitative analysis of lung density was published (16). Typical histograms for inspiration and expiration were presented and offered the possibility to obtain quantitative information from lung CT. The method was demonstrated to be reproducible, but the authors already denoted limitations caused by artifacts and incomplete inspiration. In almost 40 years, these limitations still play an important role. Moreover, the introduction of multiple scanning techniques, reconstruction filters, scanner models and manufacturers did not improve this either. As a result, the quantification of emphysema (but also air trapping), which is still mainly based on thresholding, is subject to a great number of variables.

The main inconvenience in lung quantification originates from the organ itself; the lung is not a homogeneous substance, but a structured organ with changing density values caused by different vascular, interstitial, and air portions. Lung density can decrease with an increase in the amount of alveolar space (as in emphysema), but can also increase with increasing interstitial space (i.e., in fibrosis). Both processes can appear in the same damaged lung, which indicates the need for regional information.

A second difficulty of the lung that no other organ of the human body does, is that its density changes in relation to its function. With maximum inspiration and expiration, a striking alteration of lung density values is seen, which makes it necessary to standardize the functional condition of the lung during CT acquisition in order to achieve reproducible values. As reproducing maximum inspiration seems to be fairly accessible, exhaling at a constant maximum degree is less well reproducible (17).

Will artificial intelligence (AI) amplify the introduction of quantitative CT analyses in clinical practice? Probably. AI enables more precise segmentation of fissures, lobes, and the broncho-vascular tree, which is an essential step for image quantification (18,19). AI can help in detecting early parenchymal injury before irreversible damage appears whereby knowledge on early parenchymal changes in COPD can be acquired. By linking this to genetic loci, functional data on the genetic and molecular basis of COPD will be enabled (20).

Although AI systems are mainly trained with human labels, AI delivers beyond human expertise as it comes to recognition tasks and classification performance (21). AI can interpret data without prior hypotheses and can explore new phenotypes by connecting imaging phenotypes to genetic and molecular features. This however leads to more empirical data and not to implementation in clinical use. A challenge with AI is that it is trained with specific samples of a specific population and further replication studies are needed to define its true performance in clinical practice. This requires careful data sharing infrastructures that preserve data integrity and privacy. Another challenge includes our urge to understand AI approaches and the dislike of the ‘black box’, although this is not always grounded as parameters are available and can be inspected.

Quantitative CT evaluation can successfully identify emphysema, expiratory airflow obstruction, airway wall thickening, and measure lung movement by using dynamic-ventilation CT, but perhaps this does not fully capture the information available from visual subtyping and other smoking related lung changes. Visually, radiologists can encounter quality issues and look beyond noise, reconstruction filter, artifacts, etc. In addition, a radiologist takes into consideration the patients’ clinical traits and history. Subtypes have been defined with visual but no quantitative
emphysema, which could be a result of regional emphysema or an accompanying increase in lung density, highlighting the importance of a radiologists’ evaluation (22). A drawback of visual scoring is its subjectivity and need for experience. One study showed that visual assessment of the presence of COPD on a chest CT is less sensitive than PFT (23). Considering all things, PFT, visual and quantitative CT evaluation are currently regarded as complementary methods to assess COPD.

For now, as it comes to the assessment of COPD phenotypes, beauty is in the eye of the beholder. To be a beholder, one has to pay attention and be aware of other helpful techniques. In other words, the beauty does not exist on its own but is created by the observer.

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