Optimal Fat Suppression in Head and Neck MRI: Comparison of Multipoint Dixon with 2 Different Fat-Suppression Techniques, Spectral Presaturation and Inversion Recovery, and STIR

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ABSTRACT

BACKGROUND AND PURPOSE: Uniform complete fat suppression is essential for identification and characterization of most head and pathology. Our aim was to compare the multipoint Dixon turbo spin-echo fat-suppression technique with 2 different fat-suppression techniques, including a hybrid spectral presaturation with inversion recovery technique and an inversion recovery STIR technique, in head and neck fat-suppression MR imaging.

MATERIALS AND METHODS: Head and neck MR imaging datasets of 72 consecutive patients were retrospectively reviewed. All patients were divided into 2 groups based on the type of fat-suppression techniques used (group A: STIR and spectral presaturation with inversion recovery gadolinium-T1WI; group B: multipoint Dixon T2 TSE and multipoint Dixon gadolinium-T1WI TSE). Objective and subjective image quality and scan acquisition times were assessed and compared between multipoint Dixon T2 TSE versus STIR and multipoint Dixon gadolinium-T1WI TSE versus spectral presaturation with inversion recovery gadolinium-T1WI using the Mann-Whitney U test.

RESULTS: A total of 64 patients were enrolled in the study (group A, n = 33 and group B, n = 31). Signal intensity ratios were significantly higher for multipoint Dixon T2 and gadolinium-T1WI techniques compared with STIR (P < .001) and spectral presaturation with inversion recovery gadolinium-T1WI (P < .001), respectively. Two independent blinded readers revealed that multipoint Dixon T2 and gadolinium-T1WI techniques had significantly higher overall image quality (P = .022 and P < .001) and fat-suppression grades (P < .013 and P < .001 across 3 different regions) than STIR and spectral presaturation with inversion recovery gadolinium-T1WI, respectively. The scan acquisition time was relatively short for the multipoint Dixon technique (2 minutes versus 4 minutes 56 seconds for the T2-weighted sequence and 2 minutes versus 3 minutes for the gadolinium-T1WI sequence).

CONCLUSIONS: The multipoint Dixon technique offers better image quality and uniform fat suppression at a shorter scan time compared with STIR and spectral presaturation with inversion recovery gadolinium-T1WI techniques.

ABBREVIATIONS: AP = anteroposterior; CHESS = chemical shift selective suppression; FS = fat suppression; Gad-T1WI = gadolinium-T1WI; mDixon = multipoint Dixon; SPIR = spectral presaturation with inversion recovery

Uniform and complete fat suppression (FS) is indispensable for accurate diagnosis and characterization of head and neck pathologies. Various FS MR imaging techniques are available clinically, each with its own advantages and disadvantages. Commonly used FS MR imaging techniques include STIR, chemical shift selective suppression (CHESS), hybrid methods such as spectral presaturation with inversion recovery (SPIR; Phillips Healthcare, Best, the Netherlands), spectral attenuated inversion recovery, and a more recent chemical shift method, the multipoint Dixon (mDixon Technique; Phillips Healthcare).

The STIR technique nulls the fat signal using a 180° inversion pulse as an initial excitation pulse, followed by a subsequent 90° pulse at a specified inversion time (approximately 160–180 ms for a 1.5T magnet). The CHESS technique uses a radiofrequency pulse tuned to the fat-resonance frequency together with a spoiler gradient, which saturates fat signal and thus leaves only water protons to produce signal. SPIR is a hybrid FS technique that combines the fat selectivity of CHESS and uses an inversion radiofrequency pulse like that in the STIR technique. Never-
The more recently developed mDixon technique is in-

杜绝 acquisition times.

while preserving the desired image contrast at reduced scan

sensitive to magnetic field (both B0 and B1) inhomogeneity

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MATERIALS AND METHODS

The ethics committee of our institution (University of Wash-

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countability Act–compliant study. We retrospectively re-

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olinium administration for various clinical indications, be-

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criterion was that these patients also have a CT examination of

the neck within 3 months before or after the MR imaging

study. The CT data were used to quantify body habitus. Pa-

ients with poor renal function (glomerular filtration rate of

<30) and suboptimal image quality secondary to patient mo-

tion artifacts were excluded from the study. None of the en-

rolled patients had cervical spine fusion hardware. Systematic

changes were made in the institutional head and neck MR im-

aging protocol during the study time period so that the previ-

ously obtained STIR/SPIR combination of FS techniques was

gradually switched to the evaluated mDixon FS techniques.

The enrolled subjects were divided into 2 groups (group A and

group B) based on the combination of FS techniques used for

the corresponding T2-weighted sequence and Gad-T1WI se-

quence. In group A subjects, STIR images were acquired as a

T2-weighted sequence and SPIR images were acquired as the

post Gad-T1WI FS technique. In group B subjects, a 2D

mDixon spin-echo (2D-3-point mDixon TSE) technique was

used to suppress fat signal in both T2-weighted and post-Gad-

T1WI sequences.

Data Acquisition

All MR imaging scans were obtained on a 3T scanner (Achieva; Phil-

ips Healthcare). As per our institution protocol, we obtained the

following MR imaging sequences: axial, sagittal, and coronal T1WI;

and axial and coronal fluid-sensitive sequences with fat suppression

(axial STIR and coronal CHESS FS T2WI or axial and coronal

mDixon FS T2WI), followed by gadolinium-enhanced (gadoteridol,

ProHance, 279.3 mg/mL; Bracco Diagnostics, Princeton, New Jer-

cy) axial and coronal T1WI with FS sequences (SPIR or mDixon). Parameters used for STIR, SPIR FS Gad-T1WI, mDixon FS T2WI,

and mDixon FS Gad-T1WI are summarized in Table 1.

Data Analysis

Objective Analysis. All objective measurements were performed by a fellowship-trained neuroradiologist with 10 years of cumu-

lative experience in head and neck imaging. As the surrogate mea-

sure of a patient’s body size, the maximum anteroposterior (AP)

neck diameter at the level of mandible (parallel to the C2–3 inter-

vertebral disc), minimum AP diameter at the midneck level (par-

allel to the C4–5 intervertebral disc), and maximum transverse

shoulder width (Fig 1) were measured on the neck CT topogram.

The ratios of AP neck diameter at the level of the mandible to the

AP diameter at the midneck level and shoulder width to AP diam-

eter of the midneck were calculated for each subject and were

compared between the 2 groups (groups A and B).

Signal intensity of the spinal cord and subcutaneous fat was

measured (Fig 2) by placing a circular ROI measuring 5–10 mm in

diameter on an axial image at 2 different levels (submandibular

region and supracleavicular region) on all sequences. To normalize

the relative fat signal intensity, we calculated the signal intensity

ratio between the spinal cord and subcutaneous fat at both levels

for each sequence. The ratios were compared between STIR and

mDixon FS T2 TSE and between SPIR FS Gad-T1WI and mDixon

FS Gad-T1WI TSE, respectively.

Subjective Analysis. Two fellowship-trained and board-certif-

ied neuroradiologists, each with 12 years of experience in in-

Table 1: Parameters used for different fat-suppression sequences on a 3T scanner

| Parameter                        | Axial STIR | Axial T2WI | Axial Gad-T1WI | Axial Gad-T1WI |
|----------------------------------|------------|------------|----------------|----------------|
|                                  | TSE        | mDixon TSE | SPIR TSE       | mDixon TSE     |
| Coil                             | 16 Channel | 16 Channel | 16 Channel     | 16 Channel     |
| SENSE N/V                        |            |            |                |                |
| TR/TE                            | 3000/15 ms | 3000/80 ms | 600/9.2 ms     | 500/10 ms      |
| Section thickness/intersection gap| 3/1 mm     | 3/1 mm     | 3/1 mm         | 3/1 mm         |
| No. of axial images F5 technique  | 40         | 40         | 40             | 40             |
| Acquisition matrix               | 200 × 141  | 232 × 232  | 288 × 196      | 204 × 199      |
| NEX                              | 2          | 1          | 1              | 1              |
| Acquisition time                 | 4 min, 56 sec | 2 min, 2 sec | 3 min, 2 sec | 2 min, 8 sec |
| Parallel imaging                 | Yes        | Yes        | Yes            | Yes            |
| Gadolinium contrast              | N/A        | N/A        | 0.1 mmol/kg gadodiamine (Gd-DTPA) (ProHance) | 0.1 mmol/kg gadodiamide (Gd-DTPA) (ProHance) |

Note: SENSE indicates sensitivity encoding; N/A, not applicable; NV, NeuroVascular.

A Achieva; Philips Healthcare.
ratings of 2 readers were averaged to compare the groups. A permutation test, clustered by patient, was used to compare the presence of dental amalgam susceptibility artifacts as rated by both readers separately between sequence groups. Interreader agreement of the subjective ratings was summarized using the Cohen \( \kappa \) (linearly weighted for 5-point scales and unweighted for binary variables) and percentage agreement. Percentage agreement for the 5-point scales was calculated after combining the ratings into a 3-point scale: 1–2, 3, and 4–5. Bias in ratings between the readers was assessed using the Wilcoxon signed rank test. A \( P \) value of < .05 was considered statistically significant. All statistical calculations were conducted with the statistical computing language R (Version 3.1.1; http://www.r-project.org/).

RESULTS

Patient Demographics

Group-based patient demographics are summarized in Table 2. A total of 64 patients met the inclusion criteria, following exclusion of 8 patients (due to suboptimal MR imaging due to motion artifacts \([ n = 5]\) and lack of intravenous gadolinium-based contrast agent administration \([ n = 3]\)). Group A comprised 33 patients (10 women), while group B comprised 31 patients (11 women).

There was no statistically significant difference in the age (mean, 61 ± 15 years versus 55 ± 17 years; \( P = .15 \)) or sex (\( P = .79 \)) distribution, between the groups. There was no significant difference in body habitus, represented by the ratio between groups, of shoulder width–to–mandibular region AP neck diameter at the C2–3 level (1.53 ± 0.16 versus 1.48 ± 0.15 for groups A and B, respectively; \( P = .35 \)); and the ratio of shoulder width–to–midneck AP diameter at the C4–5 level (3.21 ± 0.36 versus 3.16 ± 0.40, for groups A and B, respectively; \( P = .88 \)).

Objective Assessment

Objective image-quality measurements are summarized in Table 3. Signal intensity ratios measured between the spinal cord and subcutaneous fat at the submandibular and supraclavicular levels were significantly higher for the mDixon technique. For T2-weighted sequences (STIR versus mDixon T2-weighted TSE), the ratio measured 3.5 ± 3.4 versus 5.7 ± 1.6, respectively \(( P < .001)\) at the submandibular level and 3.3 ± 3.4 versus 7.4 ± 2.4, respectively \(( P < .001)\) at the supraclavicular level. Similarly, in the post-gadolinium-enhanced FS T1-weighted sequence (SPIR Gad-T1WI versus mDixon Gad-T1WI TSE), the ratio measured 0.9 ± 0.7 versus 3.7 ± 1.4, respectively \(( P < .001)\) at submandibular level and 0.5 ± 0.3 versus 4.3 ± 2.0, respectively \(( P < .001)\) at supraclavicular level.

Statistical Analysis

Variables were summarized as mean ± SD or count (percentage). The sequence groups were compared using the Mann–Whitney \( U \) test. For the analysis of subjective image-quality ratings, the

FIG 1. Lateral (A) and frontal (B) projections of CT topogram images with measurements of anteroposterior diameter at the level of C2–3 and C4–5 and transverse diameters at the shoulder.

FIG 2. Gadolinium-enhanced T1-weighted MR images with SPIR (A) and mDixon (B) techniques for fat suppression. ROIs are placed on the spinal cord and fat to obtain a signal intensity ratio.
subjective assessment of image quality, fat suppression, and  
susceptibility artifacts.

### Table 4: Subjective assessment of image quality, fat suppression, and susceptibility artifacts

| Variable                        | Sequence Group | Group B (n = 31) | Group A (n = 33) | P Value<sup>b</sup> |
|---------------------------------|----------------|------------------|------------------|---------------------|
| **T2WI/STIR images**            |                |                  |                  |                     |
| Overall image-quality grade     |                | 3.9 ± 0.5        | 3.6 ± 0.7        | .022                |
| Fat-saturation grade            |                |                  |                  |                     |
| Maxillary region                |                | 4.6 ± 0.4        | 4.3 ± 0.5        | .013                |
| Mandibular region               |                | 4.4 ± 0.5        | 4.0 ± 0.6        | .007                |
| Lower neck region               |                | 4.7 ± 0.4        | 4.3 ± 0.4        | .001                |
| Dental amalgam susceptibility artifacts (%) |                | 38.7% | 22.7% | .056 |
| Post-Gad-T1WI images            |                |                  |                  |                     |
| Overall image-quality grade     |                | 4.0 ± 0.4        | 2.6 ± 0.6        | <.001               |
| Fat-saturation grade            |                |                  |                  |                     |
| Maxillary region                |                | 4.8 ± 0.3        | 3.8 ± 0.7        | <.001               |
| Mandibular region               |                | 4.7 ± 0.3        | 2.8 ± 0.5        | <.001               |
| Lower neck region               |                | 4.8 ± 0.3        | 1.4 ± 0.7        | <.001               |
| Dental amalgam susceptibility artifacts (%) |                | 37.1% | 31.8% | .50 |

<sup>a</sup> Two readers averaged. Values are mean ± SD unless otherwise specified.  
<sup>b</sup> Mann-Whitney U test comparing average ratings or permutation test (clustered by patient) for susceptibility artifacts.

Subjective Assessment

The averages of the 2 readers’ subjective assessments of the uniformity of fat suppression and overall image quality for groups A and B are summarized in Table 4.

Fat Suppression. The average scores from both the readers for fat suppression at all 3 levels (maxillary, mandibular, and lower neck region) were significantly higher for mDixon T2-weighted FS TSE (mean, 4.4–4.7) compared with STIR (mean, 4.0–4.3; P < .013 for all regions) (Fig 3) and mDixon Gad-T1WI FS TSE sequences (mean, 4.7–4.8) compared with SPIR Gad-T1WI (mean, 1.4–3.8, P < .001 for all regions) (Figs 4 and 5).

Overall Image Quality. Similarly, the 2 readers’ average scores for overall image quality were significantly higher for mDixon T2-weighted FS TSE than for STIR (mean, 3.9 versus 3.6; P = .022) and mDixon Gad-T1WI FS TSE sequences (mean, 4.0 versus 2.6; P < .001).

Susceptibility Artifacts Related to Dental Amalgam. There was no significant difference in the percentage of subjects with susceptibility artifacts related to dental amalgam between the 2 groups for both fluid-sensitive sequences (38.7% versus 22.7%, P = .056) and post-Gad-T1WI sequences (37.1% versus 31.8%, P = .5).

Interreader Agreement

The percentage agreement for the uniformity of fat suppression between the readers was >87% for group B patients (On-line Table), though the corresponding κ values ranged from 0.05 to 0.15. Across all 3 stations, readers gave ratings of only 4–5 for 87%–100% of cases, so there was a limited range of ratings for the κ assessment. Group A interreader agreement varied between 25% and 91% (On-line Table), with corresponding κ values from −0.07 to 0.58. Across the 3 stations, readers used only 2 different levels 67%–99% of the time.

Scan Acquisition Times. The acquisition times were shorter for the mDixon techniques compared with STIR (2 minutes versus 4 minutes 56 seconds) and SPIR (2 minutes versus 3 minutes).

DISCUSSION

In this retrospective study, we enrolled 33 subjects who underwent MR imaging with a STIR and SPIR combination of fat-suppression techniques and 31 subjects with mDixon as the fat-suppression technique.
pression technique. The subjects were matched for age, sex, and surrogate imaging markers of body habitus in the area of interest. In this study group, we demonstrate that the objective image quality measured for signal intensity ratios (spinal cord to subcutaneous fat signal) was significantly higher for the Dixon technique compared with STIR and SPIR. This finding clearly indicates that the mDixon technique provides better fat suppression, even in the areas where other fat-suppression techniques failed due to technical reasons. In the subjective assessment, readers scored the mDixon technique significantly higher for uniformity of fat suppression and overall image quality. An additional minor advantage with the mDixon technique is relatively shorter scan acquisition times. Our study results are in concordance with previous studies comparing the 3-point mDixon with the CHESS fat-suppression technique in spine, neck, and orbit imaging.

The main disadvantages associated with STIR include suppression of signals from tissues with similar T1 values (such as subacute hematoma and gadolinium-enhanced tissues). In addition, fewer sections were obtained for a given TR compared with the spin-echo technique because a certain portion of the time is consumed by the TI and TE of STIR. STIR is considered sensitive to spatial nonuniformity of the applied radiofrequency pulse (unless an adiabatic pulse is used). If the strength of the radiofrequency pulse varies from one position to another within the subject, then the tip angle of the inversion pulse, and hence the quality of fat suppression, will also vary with position. Finally, the uniformity of fat suppression may depend on selection of an appropriate TI. In addition, STIR alters signal from all tissues and thus decreases the contrast as well as the signal-to-noise ratio. CHESS and its derivative SPIR hybrid techniques require a homogeneous magnetic field for uniform fat suppression. They fail to suppress fat signal around susceptibility distortions due to metallic hardware, sinuses, and skull base or in the regions far from the isocenter. They also increase the specific absorption rate to the patient and scan times due to use of an extra presaturation pulse and dephasing gradient. Uniformity of FS by CHESS/SPIR techniques is heavily dependent on homogeneity of the main magnetic field (B0) and radiofrequency magnetic field (B1); hence, nonuniform fat suppression occurs farther away from the isocenter of B0. Another important factor described to explain the nonuniformity of FS in the CHESS/SPIR technique in areas with a sharp variation of the shape of anatomic structures such as the floor of the mouth and the supraclavicular region is the so-called bulk susceptibility phenomenon.

The mDixon technique for FS was first described by Dixon in 1984. This is a spectroscopic imaging technique that relies on water and fat chemical shift differences. The original technique was designed to acquire 2 sets of images, one with water and fat signal being in-phase and the other acquired when water and fat signals are at 180° out-of-phase (referred to as the “2-point Dixon technique”). Using these 2 sets of images, one can generate water-only and fat-only images. The water-only images serve as effective fat suppression. The main advantage of this technique is that it is relatively insensitive to B0 inhomogeneity but not completely immune to it because sometimes the B0 inhomogeneity can manifest as phase errors. The fundamental assumption of the mDixon technique is that water and fat are the only 2 signal-contributing chemical species in the object to be imaged. Under this assumption, it is believed that water or fat each has only a single spectral peak. This assumption may be true for water but not for fat because fat is known to contain many spectral components. The B0 inhomogeneity and other system imperfections contribute to phase error results in signal contributions to both water-only and fat-only images, even from the pixels containing only fat tissue.

Failure of phase correction usually leads to swapping of water and fat assignments for the affected pixels, which can sometimes present a “pseudomass” appearance or incomplete fat suppression. Correlating with both water-only and fat-only images may help reduce this misinterpretation. A more recent technical advance, the 3-point Dixon technique, acquires an addi-

FIG 3. Axial STIR (A and B) and mDixon T2-weighted (C and D) MR images. Note incomplete fat suppression (asterisks) in the maxillary and supraclavicular regions on the STIR technique and complete uniform fat suppression (arrowheads) in the submandibular and supraclavicular regions on the mDixon technique.
third set of images along with the traditionally acquired 0° and 180°; it can be either /H11002 180°, 0, 180° or 0, 180°, 360°. This additional image set helps determine and correct the phase error. 13-17

Study Limitations

There are several limitations to this study: 1) It is a retrospective study and hence has a limitation of selection bias; 2) it is a relatively small cohort of patients, particularly when considering comparison for 3 different techniques; and 3) a combination of different FS techniques was used in 2 separate populations (groups A and B). This is particularly important because uniformity of FS in certain techniques such as CHESS and its modifications (SPIR) depend heavily on the patient’s body habitus and on patient position in the magnet. In our study, we think the contribution of patient-related factors was not significant, considering that there was no statistically significant difference in the demographics and patient body habitus (in the area of interest) between the groups. Fourth, lesion detectability and conspicuity were not assessed due to heterogeneity in the scan indications. Not all patients had a focal lesion, and when a focal lesion was present, no 2 lesions were comparable due to heterogeneity in the type of disease, location, and stage of treatment. Fifth, there was some disagreement between readers during the subjective assessment; however, ratings by both readers showed similar trends between groups A and B, and the readers typically used only 2 different adjacent rating levels at each station. Therefore, while readers may have disagreed on individual ratings, they usually agreed that ratings were high (4–5), low (1–2), or moderate (2–3 or 3–4).

CONCLUSIONS

The mDixon technique provides more uniform fat suppression and improved image quality compared with other commonly used FS techniques such as STIR and SPIR, while reducing sequence acquisition times in head and neck MR imaging.

REFERENCES

1. Del Grande FD, Santini F, Herzka DA, et al. Fat-suppression techniques for 3-T MR imaging of the musculoskeletal system. Radiographics 2014;34:217–33 CrossRef Medline
2. Ma J. Dixon techniques for water and fat imaging. J Magn Reson Imaging 2008;28:543–58 CrossRef Medline
3. Ma J, Singh SK, Kumar AJ, et al. T2-weighted spine imaging with a fast three-point Dixon technique: comparison with chemical shift selective fat suppression. J Magn Reson Imaging 2004;20:1025–29 CrossRef Medline
4. Ma J, Jackson EF, Kumar AJ, et al. Improving fat-suppressed T2-weighted imaging of the head and neck with 2 fast spin-echo Dixon

FIG 4. Gadolinium-enhanced axial T1-weighted MR images with SPIR (A and B) and mDixon (C and D) techniques for fat suppression. Note incomplete fat suppression (asterisks) in the submandibular and supraclavicular regions on the SPIR technique and complete uniform fat suppression (arrowheads) in similar regions on the mDixon technique.

FIG 5. Gadolinium-enhanced coronal T1-weighted MR images with SPIR (A) and mDixon (B) techniques for fat suppression. Note incomplete fat suppression (dark asterisk) in the supraclavicular regions on the SPIR technique and complete uniform fat suppression (white asterisk) in similar regions on the mDixon technique.
5. Rybicki FJ, Mulkern RV, Robertson RL, et al. Fast three-point Dixon MR imaging of the retrobulbar space with low-resolution images for phase correction: comparison with fast spin-echo inversion recovery imaging. *AJNR Am J Neuroradiol* 2001;22:1798–802

6. Tien RD. Fat-suppression MR imaging in neuroradiology: techniques and clinical application. *AJR Am J Roentgenol* 1992;158:369–79 CrossRef Medline

7. Bydder GM, Steiner RE, Blumgart LH, et al. MR imaging of the liver using short TI inversion recovery sequences. *J Comp Assist Tomogr* 1985;9:1084–89 CrossRef Medline

8. Bydder GM, Young IR. MR imaging: clinical use of the inversion recovery sequence. *J Comp Assist Tomogr* 1985;9:659–75 CrossRef Medline

9. Shuman WP, Baron RL, Peters MJ, et al. Comparison of STIR and spin-echo MR imaging at 1.5 T in 90 lesions of the chest, liver, and pelvis. *AJR Am J Roentgenol* 1989;152:853–59 CrossRef Medline

10. Dixon WT. Simple proton spectroscopic imaging. *Radiology* 1984;153:189–94 CrossRef Medline

11. Hardy PA, Hinks RS, Tkach JA. Separation of fat and water in fast spin-echo MR imaging with the three-point Dixon technique. *J Magn Reson Imaging* 1995;5:181–85 CrossRef Medline

12. Low RN, Austin MJ, Ma J. Fast spin-echo triple echo Dixon: initial clinical experience with a novel pulse sequence for simultaneous fat-suppressed and nonfat-suppressed T2-weighted spine magnetic resonance imaging. *J Magn Reson Imaging* 2011;33:390–400 CrossRef Medline

13. Yeung HN, Kormos DW. Separation of true fat and water images by correcting magnetic field inhomogeneity in situ. *Radiology* 1986;159:783–86 CrossRef Medline

14. Glover GH, Schneider E. Three-point Dixon technique for true water/fat decomposition with B0 inhomogeneity correction. *Magn Reson Med* 1991;18:371–83 CrossRef Medline

15. Glover GH. Multipoint Dixon technique for water and fat proton and susceptibility imaging. *J Magn Reson Imaging* 1991;1:521–30 CrossRef Medline

16. Maas M, Hollak CE, Akkerman EM, et al. Quantification of skeletal involvement in adults with type I Gaucher’s disease: fat fraction measured by Dixon quantitative chemical shift imaging as a valid parameter. *AJR Am J Roentgenol* 2002;179:961–65 CrossRef Medline

17. Wang Y, Li D, Haacke EM, et al. A three-point Dixon method for water and fat separation using 2D and 3D gradient-echo techniques. *J Magn Reson Imaging* 1998;8:703–10 CrossRef Medline