Cardiovascular function, compliance, and connective tissue remodeling in the turtle, *Trachemys scripta*, following thermal acclimation

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Keen AN, Shiels HA, Crossley DA 2nd. Cardiovascular function, compliance, and connective tissue remodeling in the turtle, *Trachemys scripta*, following thermal acclimation. *Am J Physiol Regul Integr Comp Physiol* 311: R133–R143, 2016. First published April 13, 2016; doi:10.1152/ajpregu.00510.2015.—Low temperature directly alters cardiovascular physiology in freshwater turtles, causing bradycardia, arterial hypotension, and a reduction in systemic blood pressure. At the same time, blood viscosity and systemic resistance increase, as does sensitivity to cardiac preload (e.g., via the Frank-Starling response). However, the long-term effects of these seasonal responses on the cardiovascular system are unclear. We acclimated red-eared slider turtles to a control temperature (25°C) or to chronic cold (5°C). To differentiate the direct effects of temperature from a cold-induced remodeling response, all measurements were conducted at the control temperature (25°C). In anesthetized turtles, cold acclimation reduced systemic resistance by 1.8-fold and increased systemic blood flow by 1.4-fold, resulting in a 2.3-fold higher right to left (R-L; net systemic) cardiac shunt flow and a 1.8-fold greater shunt fraction. Following a volume load by bolus injection of saline (calculated to increase stroke volume by 5-fold, ~2.2% of total blood volume), systemic resistance was reduced while pulmonary blood flow and systemic pressure increased. An increased systemic blood flow meant the R-L cardiac shunt was further pronounced. In the isolated ventricle, passive stiffness was increased following cold acclimation with 4.2-fold greater collagen deposition in the myocardium. Histological sections of the major outflow arteries revealed a 1.4-fold higher elastin content in cold-acclimated animals. These results suggest that cold acclimation alters cardiac shunting patterns with an increased R-L shunt flow, achieved through reducing systemic resistance and increasing systemic blood flow. Furthermore, our data suggests that cold-induced cardiac remodeling may reduce the stress of high cardiac preload by increasing compliance of the vasculature and decreasing compliance of the ventricle. Together, these responses could compensate for reduced systolic function at low temperatures in the slider turtle.

Heart; in vivo; blood flow; blood pressure; cardiac preload; stiffness; collagen; elastin

Reductions in ambient temperature have direct (i.e., Q₁₀; the rate of change over 10°C) and immediate effects on the ectotherm heart and cardiovascular system. This response to low temperature is clear in freshwater turtles, resulting in decreased heart rate (fH), cardiac twitch force, cardiac output (Q_\text{total}), and ventricular power output (15, 27). However, cardiac stroke volume (VStot) is maintained at low temperatures, partly by reduced end-systolic volume and increased diastolic filling due to changes in vascular resistance, and the sensitivity of the turtle heart to cardiac preload is increased (15, 27). These temperature-induced responses and the direct effect of temperature on blood viscosity may alter hemodynamic load on the heart (44, 56, 62). If prolonged, these physical and functional changes may trigger a dynamic remodeling of the passive and active properties of the cardiovascular system (62, 63).

Freshwater slider turtles (*Trachemys scripta*) spend winter in water in a state of periodic inactivity. Following cold acclimation slider turtles exhibit a compensatory increase in cardiac muscle twitch force and maximal isometric force, as well as a suppression of cholinergic inhibition, slower action potential upstroke, and longer action potential duration, accompanied by a dissipation of resting membrane potential (28, 51, 59, 62, 64). However, heart and ventricular mass do not increase (51). With the increased sensitivity to cardiac preload (15) and ability for a large Frank-Starling response (19), it has been suggested that VStot has the potential to increase fivefold in diving slider turtles (6).

Cardiac parameters of warm- and cold-acclimated turtles have been previously reported in a number of studies, which are in general agreement that following cold acclimation fH, Q_\text{total}, and Psys are decreased while VStot, systemic resistance (Rsys) and hematocrit are increased (27, 51, 62, 64). However, these studies were performed at the turtle’s acclimation temperature (i.e., ~5 and 25°C for cold and control, respectively). While this experimental methodology allows determinations of cardiac function at the acclimation temperature, the physical changes to the cardiovascular system caused by cold acclimation are difficult to isolate from the direct effect of cold temperature. Studies in rainbow trout have shown significant structural remodeling of the cardiovascular system, which persists in the absence of the direct effects of low temperature (39, 42). Therefore, to differentiate a remodeling response from the direct effect of temperature, cardiovascular function must be assessed at a common “test” temperature.

Our objective was to determine whether prolonged temperature acclimation caused remodeling of the freshwater red-eared slider turtle (*Trachemys scripta*) cardiovascular system. To differentiate the direct effect of temperature, and focus on the longer term remodeling response of the cardiovascular system, animals were acclimated to a cold (5 ± 0.3°C) or control temperature (25 ± 0.3°C), but all experiments were conducted at the control temperature (of 25 ± 0.3°C). We assessed in vivo cardiac parameters in anesthetized animals after a period of postsurgical stabilization and then in response to a bolus injection (mean = 2.2 ± 0.4% of total blood volume) of saline directly into the jugular vein. Our first hypothesis was that chronic cold would reduce Q_\text{total}, increase VStot, and decrease Psys. Our second hypothesis was that cold acclimation would dampen the cardiac response to increased cardiac preload. As turtles have incomplete ventricular sepa-
ration of venous and arterial circulations, allowing blood flow to bypass or partially bypass either systemic or pulmonary circulation (29, 30, 32), we were particularly interested in cardiac shunt flow \( (Q_{\text{shunt}}) \) patterns. We further investigated the physical properties of the ventricle hypothesizing that cold acclimation would cause an increase in passive stiffness of the ventricle, which would be reflected in an increased collagen deposition. We found that \( Q_{\text{shunt}} \) patterns were altered following cold acclimation, with a right to left (R–L; net systemic) \( Q_{\text{shunt}} \) achieved by reducing \( R_{\text{sys}} \) and, therefore, increasing \( Q_{\text{sys}} \). Furthermore, it appears that cold-induced cardiovascular remodeling increases ventricular stiffness and systemic vascular compliance, which reduces the stress of high blood volume load and may compensate for decreased systemic function at low temperatures.

**MATERIALS AND METHODS**

**Experimental animals and acclimation.** Male and female red-eared sliders (Trachemys scripta, Schaeppf; \( n = 20 \); mean body mass = 1.352 ± 69 g) were obtained from Lake Lewisville, TX, and transported to the University of North Texas. Here, they were housed in 50 L plastic containers (dimensions 50 × 50 × 100 cm) containing freshwater at a temperature of 25 ± 0.3°C on a 12:12-h light-dark cycle. Water quality was maintained by 100% water changes twice a week and all animals were fed three times per week on commercial reptile feed (Aquatic turtle diet, Mazuri exotic animal nutrition). After 2 wk, 10 turtles were randomly assigned for cold acclimation where ambient temperature was reduced by 1°C per day until 5wk, 10 turtles were randomly assigned for cold acclimation where ambient temperature was reduced by 1°C per day until 5 ± 0.3°C was reached and turtles were maintained at this temperature for 8–12 wk before experiments. An acclimation period of >8 wk was chosen to agree with our recent studies on fish (39), where >8 wk acclimation time is necessary to ensure cardiovascular structural remodeling (18, 42). Animals selected for cold acclimation were fasted following temperature reduction. The acclimation temperatures (control at 25 ± 0.3°C; cold at 5 ± 0.3°C) were chosen based on previous literature (27, 28) to simulate summer and winter conditions. All acclimation temperatures were maintained in a walk in temperature controlled room (model IR-912LS; Percival Scientific, Perry, IA) and animals were maintained in water without an area for basking. All animals survived the acclimation protocols and there were no signs of poor health in either group. Animal care and surgical preparations adhered to the University of North Texas animal care and use protocol (Institutional Animal Care and Use Committee No. 11-007).

**Anesthesia and surgical procedure.** Before study, control animals were fasted for 1 wk. On the day of study, turtles were removed from acclimation tanks, immediately weighed, and then anesthetized via an intramuscular injection of sodium pentobarbital (50 mg/kg; Sigma-Aldrich, St. Louis, MO) while still at their acclimation temperature. The sodium pentobarbital was purchased as a powder and made as 2 ml 100% ethanol, 8 ml propylene glycol, and 10 ml saline with 1,000 mg pentobarbital. Animals were then transported to the experimental chamber (at 25 ± 0.3°C). In most cases the pedal withdrawal response ceased within 30–60 min postinjection; however, if it persisted, an additional injection (25 mg/kg) was administered. During surgery, and throughout experiments, turtles were maintained ventral side up and artificially ventilated to maintain normoxia via a tube inserted through the glottis into the trachea (model 665; Harvard Apparatus, Holliston, MA) at a rate of 24 breaths/min and a volume of 20 ml as previously reported for studies of this species (11, 13). Gas composition was controlled by rotameters (Sho-Rate Brooks Instruments Division, Hatfield, PA) and bubbled into a gas mixer to maintain hydration. Fractional \( CO_2 \) (\( F_{CO_2} \)) was maintained at 3 kPa to mimic partial pressure of \( CO_2 \) in arterial blood (\( P_{CO_2} \)) (11, 22). The ventilated gas mixture (\( F_{O_2} = 0.21, F_{CO_2} = 0.03, \) balance \( N_2 \)) was checked regularly using a S-3A1 oxygen analyzer and a CD-3A carbon dioxide analyzer (Ametek, Berwyn, PA).

To expose the central vascular blood vessels, a 5 × 5 cm section of the plastron was cut away using a bone saw. The pectoral muscles and connective tissue were gently loosened from the excised piece and bleeding from small superficial vessels stopped by cauterization. For measurements of blood flows, 1- to 1.5-cm sections of all of the major outflow vessels of the heart were freed from connective tissue by blunt dissection, taking care not to damage any smaller branching vessels or perforate the pericardium. 2S transit-time ultrasonic blood flow probes (Transonic Systems, Ithica, NY) were fitted around all of the major outflow vessels. The first around the common pulmonary artery (\( C_p \)), the second around the left aorta (\( L_Aa \)), the third around both the left carotid and subclavian arteries (\( L_Ca \) and \( L_Sca \)) and the final around the right aortic bundle (\( R_Aa \)) (Fig. 1A shows the major vessels as a histological section) (69). After flow probe placement, a small incision was made in the left side of the neck and the left carotid artery and exterior jugular vein were exposed by blunt dissection. Both vessels were occlusively cannulated with polyethylene tubing (PE50) containing heparinized (50 units/ml) saline (0.9% NaCl) and the incision was sutured closed. Finally, a small incision was made in the pericardium to expose the apex of the heart. During each heartbeat, the separation of the cavum arteriosum and cavum venosum could be visualized. A small hole was made in the heart wall, into the cavum arteriosum, using a 28-gauge needle, and polyethylene tubing (PE10) containing heparinized saline was inserted into the heart. The same process was repeated for the cavum venosum. We are confident that this method allowed for correct cannula placement; however, due to the subsequent passive filling experiments we could not verify this post mortem. All catheters were connected to pressure transducers, which were calibrated daily against a static column of water by a two-point calibration at 0 and 1 kPa. Before experimental procedures animals were left for a minimum of 1-h stabilization period. After 4 h all pressures and flows were checked to ensure they had been stable for at least 30 min; if they were not, the animals were left until they had. The total time from anesthetic dose to commencing experiments was ~4 h, during which cold-acclimated animals warmed to the control temperature.

**In vivo cardiovascular measurements.** Each catheter was attached to a disposable pressure transducer (model MLT0699; ADInstruments, Colorado Springs, CO), adjusted to sit at the same level as the animal’s heart, connected to an amplifier (Quad Bridge Amp; ADInstruments). Flow probes were connected to T206 dual channel small animal blood flow meters (Transonic Systems, Ithica, NY) for instantaneous blood flow rates. The output from the transonic meters and the pressure signal were acquired at 40 Hz using a PowerLab 16/35 data recording system (ADInstruments) and LabChart Pro software (v 7.2.5; ADInstruments).

All experiments were conducted at the control temperature of 25 ± 0.3°C. Turtle body temperature was monitored by a cloacal thermistor and a temperature probe (BAT-12 Microprobe Thermometer; Physi- temp, Clifton, NJ) placed in the chest cavity to ensure it remained at 25 ± 0.3°C throughout experiments. The control temperature was chosen as the common temperature, instead of 5 ± 0.3°C, as there is a body of literature on turtle heart function under anesthesia at ~25°C (11, 13, 36, 50). After stable pressures and flows were ensured, baseline recordings of all pressures and flows were taken for a 5-min period. During this time, average \( V_{\text{shot}} \) was calculated for each individual. Following baseline recording, a bolus injection of physiological saline (125 mN NaCl, 2.5 mM KCl, 2 mM CaCl\(_2\), 1 mM MgSO\(_4\), 1 mM NaH\(_2\)PO\(_4\), 10 mM HEPES, and 3 mM glucose at a pH of 7.7 with NaOH at room temperature) was administered via the jugular cannula. The bolus volume was calculated to increase the average stroke volume by fivefold for each particular animal, mimicking the possible increase in venous return associated with breath hold, ventilation, or movement (6, 60). Based on existing data suggesting total blood volume is ~7% of total body mass in this species.
(33), and under the assumption that 1 g body mass is equal to 1 ml blood volume, the average volume load was 2.2 ± 0.4% of total blood volume. The immediate change in pressure and flows were recorded during this period (~1 min) and then during the following sustained elevated increase in pressure and flows (~5 min). The animal was then left for ~25 min for pressure and flows to return to preinjection values, termed the recovery period, before a final 5-min recording was taken (Fig. 1B). After completion of experimental protocol, all can-

nulas and flow probes were removed, the animals were euthanized by intravenous administration of sodium pentobarbital (150 mg/kg), and the heart was excised.

Ex vivo ventricular passive pressure-volume curves. The intact isolated heart (free from cannulas) was washed in phosphate-buffered saline and placed into an organ bath containing Ringer solution (125 mM NaCl, 2.5 mM KCl, 2 mM CaCl2, 1 mM MgSO4, 1 mM NaH2PO4, 10 mM HEPES, and 3 mM glucose at a pH of 7.7 with NaOH at room temperature) at 25 ± 0.3°C to which 60 mM 2,3-butanedione monoxime (BDM) was added to prevent active cross-bridge cycling. Pressure-volume curves from ventricles of both the cold-acclimated group and control group were generated at the same common control temperature, of 25 ± 1°C, to isolate the effects of chronic remodeling on myocardial stiffness from the acute effects of temperature. A cannula containing 25 ± 0.3°C Ringer solution with BDM was fed through the left aorta into the ventricular lumen and secured, using 0-0 silk thread (Harvard Apparatus), occluding the vessel. A second cannula, containing saline solution (0.9% NaCl), was connected to a pressure transducer and fed through the common pulmonary artery into the ventricle lumen. Again the cannula was secured in place with 0-0 silk thread, occluding the vessel. The pressure transducer was calibrated daily against a static water column and recorded at 50 Hz using a PowerLab 16/35 data recording system (ADInstruments) and LabChart Pro software (v 7.2.5; ADInstruments). All other inflow and outflow vessels were occluded, using 0-0 silk thread, making the ventricle a sealed chamber with the two cannulas inside. With the use of a calibrated precision syringe pump (INFOR), Ringer solution with BDM was pumped into the ventricle at 0.05 ml/min until maximum volume was achieved, determined by a drop in the pressure trace following the protocol of Keen et al. (39).
All passive filling experiments were conducted <9 h after the original injection of sodium pentobarbital. The two atria and the ventricle were separated, their mass was determined to the nearest milligram, and they were fixed in 4% paraformaldehyde solution before being processed and embedded in paraffin wax.

Tissue histology. Fibrillar collagen and elastin content were analyzed semiquantitatively following the methodology of Keen et al. (39). Briefly, Formalin-fixed tissue samples were processed, embedded in paraffin wax, sectioned at 5 μm (Leica RM2255 microtome; Leica, Wetzlar, Germany), and mounted onto glass slides (Super frost plus; Thermo Fisher Scientific, Waltham, MA). Serial sections from each sample were stained with picro-sirus red for collagen (37) and Miller’s elastic stain for elastin (48). Picro-sirus red images were quantified using polarized light microscopy and Miller’s elastic images were quantified using bright-field microscopy. Mean fibrillar collagen and elastin contents were expressed as a percentage of total tissue cross-sectional area, excluding the epicardial surface, determined using ImageJ (57). All histological analysis was conducted blind to the acclimation group. Three tissue sections were considered for each individual to ensure consistency in measurements. On each tissue section three separate image montages were taken along transects across the full diameter of the tissue cross section.

Calculations and statistics. Pulmonary blood flow (Qpul) was determined directly based on the probe output, while total systemic blood flow (Qsys) was calculated as the sum of the blood flow recorded from the left aorta, left carotid and subclavian arteries, and the right bundle. Total blood flow (Qtotal) was the sum of Qpul and Qsys. Net cardiac shunt flow (Qshunt) was calculated as the difference between Qpul and Qsys (Qpul - Qsys); therefore, a positive Qshunt indicates a left to right (L-R; net pulmonary) shunt and a negative value indicates a right to left (R-L; net systemic) shunt (12, 43, 69). All flow data were standardized to body mass (kg). Heart rate (fH) was calculated on the basis of the instantaneous blood flow profile in the left aorta. Total stroke volume (VStot) was calculated as Qtotal/HR and systemic pressure (Psys; Fig. 2E) was determined directly based on the flow probe output, while total ventricular pressure (PVent; Fig. 2D) was calculated on the basis of the instantaneous blood flow profile in the aorta. Total stroke volume (VStot) was calculated as Qtotal/fH and standardized to body mass (kg). Systemic resistance (Rsys) was calculated as mean systemic blood pressure relative to systemic blood flow (Psys/Qsys), under the assumption that atrial pressure is zero, and standardized to body mass (kg). Ventricular contractility (dP/dt) was calculated as the maximum rate of pressure increase over six heartbeats, taken from the cannula positioned in the cavity arteriosum.

For all in vivo recordings, and calculations based on in vivo recordings, significant differences between acclimation temperatures and within groups were assessed by two-way repeated measures ANOVA/General Linear Model (GLM), with the cardiovascular parameter as the dependent variable, and stage of experiment and acclimation group as the fixed factors. When significance was found, a Sidak multiple comparisons post hoc test was conducted to assess significance between acclimation groups at each stage of the experiment. Differences between means within groups were subsequently assessed by Tukey’s multiple comparisons post hoc test. Mass parameters and differences in collagen and elastin deposition were analyzed separately by multiple unpaired t-tests for parametric data or Mann Whitney U-tests for nonparametric data, with each parameter as the test variables and acclimation group as the grouping variable. Each of these statistical analyses were performed using Prism v6.04 (GraphPad Software, La Jolla, CA).

Chamber filling volume was calculated from filling time by the equation:

\[
\text{volume (ml)} = \text{time (s)} \times \frac{0.05}{60}
\]

The effect of temperature acclimation on the pressure-volume relationship was assessed by ANCOVA with pressure as the dependent variable, volume and acclimation group as fixed factors, and body mass as the covariate, with a Tukey post hoc test for differences between groups using R (53). For all analyses, significance was considered at \( P < 0.05 \). Values are presented as mean ± SE throughout unless otherwise stated. Statistical details for each measurement are given in the figure legends.

RESULTS

Heart and chamber mass. Body mass (1,438.1 ± 115.4 vs. 1,266.4 ± 80.5 g), heart mass (3.07 ± 0.24 vs. 2.84 ± 0.211 g), left atrial mass (0.26 ± 0.034 vs. 0.24 ± 0.034 g), right atrial mass (0.40 ± 0.035 vs. 0.39 ± 0.035 g), ventricular mass (2.24 ± 0.17 vs. 2.07 ± 0.14 g), relative heart mass (0.22 ± 0.013 vs. 0.22 ± 0.009 g), and relative ventricular mass (0.16 ± 0.007 vs. 0.16 ± 0.007 g) were not different between cold-acclimated and control animals, respectively.

Effects of thermal acclimation on baseline in vivo cardiac function. Cold acclimation resulted in a 1.8-fold reduction in systemic resistance (Rsys) compared with control animals \([R^2 = 0.67, F(1,53) = 79.25, P < 0.0001; \text{Fig. 2A}]\). This reduction in Rsys contributed to a 1.4-fold increase in systemic blood flow (Qsys) in cold-acclimated compared with control animals \([R^2 = 0.38, F(1,58) = 8.69, P < 0.005; \text{Fig. 2B}]\). As there was no effect of temperature acclimation on total cardiac output (Qtotal; \text{Fig. 2C}), pulmonary flow (Qpul; \text{Fig. 2D}) or systemic pressure (Psys; \text{Fig. 2E}), both groups had a right to left (R-L; net systemic) cardiac shunt (Qshunt; \text{Fig. 2F}). Cardiac shunting occurs in turtles because they have incomplete venous separation of venous and arterial circulations, allowing blood flow to bypass or partially bypass either the systemic or pulmonary circulation. These intracardiac shunt flow (Qshunt) patterns, i.e., the direction of the blood shunt, are largely determined by vascular resistance of the systemic and pulmonary circulations (31, 50, 58). However, the combined effect of the greater Qsys and reduction in Rsys of the cold-acclimated turtles produced a 2.3-fold higher R-L Qshunt \([R^2 = 0.62, F(1,58) = 20.69, P < 0.0001] \) and a 1.8-fold greater shunt fraction compared with control \([R^2 = 0.31, F(1,58) = 7.02, P < 0.05]\). Interestingly, despite changes in blood flow distribution, we did not find an effect of temperature acclimation on maximum or minimum intraventricular pressure between two of the cava in the heart (Parteriosum and Pvenosum; \text{Fig. 3, A and B}) nor was there a change in ventricular contractility (\text{Fig. 3C}). Finally, there was no difference between resting heart rate (\( f_H \)) or total stroke volume (VStot) values between cold-acclimated and control animals (\text{Fig. 4, A and B}).

In vivo cardiovascular response to volume load. The bolus injection, designed to give a fivefold increase in venous return volume, increased VStot in both groups, which remained elevated during the sustained pressure period [for cold \([R^2 = 0.75, F(3,18) = 18.08, P < 0.0001]\) and for control \([R^2 = 0.42, F(3,18) = 4.32, P < 0.05]\); \text{Fig. 4B}]. This increase in VStot directly elevated Qtotal in both groups during the bolus injection and sustained pressure period [for cold \([R^2 = 0.72, F(3,18) = 15.39, P < 0.0001]\) and for control \([R^2 = 0.37, F(3,18) = 3.57, P < 0.05]\); \text{Fig. 2C}]. The \( f_H \) was not affected by the volume load (\text{Fig. 4A}). The increase in Qtotal translated into an increase in Qsys in both temperature groups [for cold \([R^2 = 0.72, F(3,18) = 15.48, P < 0.0001]\) and for control \([R^2 = 0.37, F(3,18) = 3.57, P < 0.0001]\); \text{Fig. 2B}] and Qpul in control animals only \([R^2 = 0.39, F(3,18) = 4.48, P < 0.05; \text{Fig. 2D}]\), reducing the net R-L shunt in cold-acclimated animals \([R^2 = 0.52, F(3,18) = 6.58, P < 0.005; \text{Fig. 2F}]\). The bolus injection caused a decrease in Rsys in both groups [for cold \([R^2 = 0.55, \text{Fig. 2A}]\).
E R-L Qshunt persisted in both acclimation groups, however, the
response to volume suggests a decrease in ventricular compli-
cation altered the pressure-volume relationship during filling
(Fig. 5 A).

Effects of thermal acclimation on the in vivo cardiovascular
response to volume load. Following the bolus injection, Rsyst
remained twofold higher in control compared with cold-accli-
amated animals during both the bolus injection and the sustained
pressure phase (P < 0.05; Fig. 2A). During both the bolus
injection and sustained pressure phase Qsys was slightly in-
creased, while Qpul and Psyst were slightly decreased by cold
acclimation compared with control (Fig. 2, B, D, and E). The
R-L Qshunt persisted in both acclimation groups, however, the
reduced Rsyst, Qpul, and Psyst combined with the increased Qsys
meant the R-L Qshunt remained more pronounced (Fig. 2F),
with a greater shunt fraction, in the cold-acclimated compared
with the control animals during both the bolus injection and
sustained pressure phase (P < 0.05). Temperature acclimation
did not influence Qtotal, Patteriosum, Pvenosum, f1, or VSys during
either the bolus injection or sustained pressure phase (Figs. 2C,
3, and 4).

Thermal remodeling of ex vivo ventricular compliance. The
maximum Parteriosum following the volume load was increased
in the cold-acclimated and reduced in the control group,
compared with baseline values. The increased pressure in
response to volume suggests a decrease in ventricular compli-
ance with cold acclimation. To assess the functional effects of
cardiac remodeling on the passive properties of the thermally
acclimated ventricle we generated ex vivo passive filling
curves from freshly isolated intact ventricles treated with BDM
at a common test temperature of 25°C. Thermal acclimation
increased stiffness in the cold compared with controls (Fig. 5A).

Thermal remodeling of connective tissue. Increased myocar-
dial stiffness can be due to a remodeling of the extracellular
matrix in both mammals and ectotherms (8, 39, 42). We used
picro-sirius red to determine fibrillar collagen deposition in the

\[ F_{(3,18)} = 7.38, P < 0.005 \] and for control [\( F_{(3,18)} = 12.93, P < 0.0001 \); Fig. 2A], but an increase in Psyst in the
control group only [\( F_{(3,18)} = 4.38, P < 0.05 \); Fig. 2E]. Maximum Parteriosum was increased in the cold-acclimated
animals; however, this was decreased in the control animals
(for cold \( F_{(3,18)} = 6.134, P < 0.05 \) and for control
\( F_{(3,18)} = 8.31, P < 0.05 \); Fig. 3A). Following the
bolus injection there was an increase in ventricular contractility
in both groups (for cold \( F_{(3,21)} = 6.58, P < 0.05 \) and for control
\( F_{(3,24)} = 22.09, P < 0.001 \); Fig. 3C). After the recovery period, Rsyst remained elevated in the
control group whereas it returned to baseline levels in the
cold-acclimated (Fig. 2A).

Fig. 2. Blood pressures and flows. In vivo
measurements of systemic resistance (Rsyst; A), systemic blood flow (Qsys; B), pulmonary
blood flow (Qpul; C), total cardiac output (Qtotal; D), systemic pressure (Psyst; E), and
net cardiac shunt flow (Qshunt = Qpul − Qsys; F) in cold-acclimated (open circles, dashed
line) and control (closed circles, solid line),
anesthetized and artificially ventilated, fresh-
waters assesssed at 25°C. Values are
displayed as means ± SE; n = 10. Flow
values have been standardized to mass for
graphical representation. *P < 0.05, signifi-
cant differences between acclimation groups;
+P < 0.05, significant changes from the
baseline value within groups during the ex-
periment [general linear model (GLM)].
turtle ventricle and major outflow vessels. Ventricular collagen content was 4.3-fold higher in cold-acclimated animals compared with controls ($R^2 = 0.69$, $P < 0.0001$; Fig. 5B), as shown by the higher degree of dark red staining, when visualized under bright-field light, and the increased number of birefringent fibers, when visualized under plane polarized light (Fig. 5, C, C1, D, and D1). We did not detect elastin in the turtle ventricular myocardium except in coronary vessels (not shown).

The major outflow vessels contain a thick layer of connective tissue that provides structural support and elastic recoil. With high cardiac preload and $V_{Stot}$ associated with cold acclimation, the balance of collagen and elastin in these vessels may be critical to vascular function (4, 24, 52). Staining the vessels with Miller’s elastic stain revealed a 1.4-fold increase in elastin content in the artery wall following cold acclimation ($R^2 = 0.51$, $P < 0.05$; Fig. 6A), which is visualized by the increased black staining of the elastic lamellae following cold acclimation compared with controls (Fig. 6, B and C, respectively). We were unable to statistically resolve differences between the acclimation groups for fibrillar collagen in the major outflow arteries (Fig. 6D). Representative bright-field images with their corresponding plane polarized light image are shown following cold acclimation in Fig. 6, E and $E_i$, respectively, and for controls in Fig. 6, F and $F_i$, respectively.

**DISCUSSION**

Ectotherms show a wide range of physiological responses to acute and chronic temperature change. Freshwater turtles endure large fluctuations in seasonal temperature in their native environments (66). These seasonal temperature changes directly affect many physiological processes, with extreme cold triggering winter long hibernation or brumation (66). Here, freshwater slider turtles were exposed to chronic cold ($\sim 5^\circ C$) to simulate a winter phenotype. In vivo cardiovascular function, ex vivo ventricular compliance, and connective tissue content of the ventricle and major outflow vessels were assessed. However, unlike previous studies, all experiments were conducted at a common control temperature ($25 \pm 0.3^\circ C$) to differentiate thermal remodeling of the cardiovascular system from the direct effects of temperature. Our findings indicate cold acclimation increased R-L $Q_{shunt}$ by a reduction in $R_{sys}$ and an increase in $Q_{sys}$. Furthermore, cold-induced cardiovascular remodeling increased ventricular stiffness during passive filling.

**Critique of the methods.** The acclimation duration in this study (>8 wk before the start of experiments) was longer than
used in a number of previous studies on freshwater turtles (12, 27, 62, 63) but was chosen to agree with the timeframe required for a cardiac remodeling response to temperature in other ectotherms (e.g., the rainbow trout) (39, 42). Second, the majority of previous studies on cold-acclimated turtle heart function were conducted on recovered animals (27, 62, 63). Anesthesia with pentobarbital blunts autonomic tone on the cardiovascular system and is, therefore, useful in assessing hemodynamic effects of central nervous system regulation (13, 36, 50). A number of studies have previously assessed cardiac function while animals remained under anesthesia (Table 1) (10, 11, 13, 21, 31, 36, 50). At warm temperatures anesthesia with sodium pentobarbital has been shown to cause a L-R (net pulmonary) shunt as it blocks the cholinergic mediated constriction of the pulmonary artery that is normally associated with apnoea (51). Third, we also continuously artificially ventilated our animals to prevent hypoxia. Lung ventilation in recovering animals is associated with an increased $f_{\text{H}}$ and $Q_{\text{pul}}$ and a reduction in the overall R-L shunt (58, 69, 71), suggested to be due to vagal and adrenergic tone (27, 30). Using a continuous artificial ventilation protocol has been shown to remove pulmonary CO$_2$ more effectively (46) than the episodic ventilation pattern seen in a nonanesthetized and unventilated animal; a series of consecutive breaths interspersed by periods of apneas causing bodily gas stores to fluctuate (22, 46, 58). However, $f_{\text{H}}$ and overall $Q_{\text{pul}}$ are not affected by this continuous ventilation pattern (46). Finally, the turtles used in this study were maintained in water throughout the acclimation period in both groups. To adjust buoyancy turtles may retain water in their urinary bladder or cloacal bursae when maintained in water for prolonged periods of time (34, 55). We did not find any difference in total body mass between control and cold-acclimated turtles, in agreement with previous studies (27, 51). However, as we did not measure body mass before and after acclimation periods we are unsure if it was altered by water retention.

The effect of thermal acclimation on systemic pressure and blood flow. Our findings suggest cold acclimation reduced $R_{\text{sys}}$, increased $Q_{\text{sys}}$, and, therefore, increased R-L $Q_{\text{shunt}}$. Previously, cold acclimation has been reported to reduce both $P_{\text{sys}}$ and systemic conductance ($G_{\text{sys}}$, $1/R_{\text{sys}}$) in turtles (12, 27, 61–63). Speculatively, this may be due to atrial natriuretic peptide (ANP), which is present in the testudine heart (65). In mammals and reptiles, ANP is released by cardiomyocytes in response to pressure or volume induced myocardial stretch and has systemic vasodilatory action (41, 49); however, it is unclear if the action of ANP is blunted by cold temperatures like some other endocrine functions (45). Vasodilation is consistent...
with previous studies that show arterial hypotension following cold acclimation when animals are studied at their acclimation temperatures (27). However, temperature is also inversely related to blood viscosity (44, 54, 56), which leads to higher viscosity at low temperatures and an overall increase in $R_{sys}$ (27, 62, 63). The overall decrease in $R_{sys}$ following cold acclimation, in the current study, suggests either a functional change in the vasculature, changes in vascular physical properties, or reduced viscosity at 25°C. However, Saunders and Patel (56) report very little difference between blood viscosities of red-eared sliders when tested at 25°C, except at very low shear rates, regardless of whether turtles were acclimated to 25 or 5°C. Furthermore, we found an increased $Q_{sys}$ when cold-acclimated animals were studied at 25°C, which differs from the findings previously reported for animals studied at 5°C (62, 63). We also report an increased elastin content found in the major outflow arteries, suggesting increased compliance and elastic recoil in these vessels. Indeed, cold acclimation may induce decreases in $R_{sys}$ via a structural change in vasculature compliance; however, further studies are needed to test this speculation experimentally.

Cardiovascular remodeling with temperature acclimation.

In both acclimation groups, a volume load of $\sim 2.2\%$ of total blood volume increased $V_{Stot}$, $P_{sys}$, and $Q_{total}$ in agreement

Table 1. In vivo cardiac parameters in anesthetized freshwater slider turtles (Trachemys scripta) at warm temperatures (~25°C)

| Variable | Cold | Control |
|----------|------|---------|
| $Q_{pul}$, ml·min⁻¹·kg⁻¹ | 31.9 | 31.1 |
| $Q_{sys}$, ml·min⁻¹·kg⁻¹ | 28.0 | 20.7 |
| $f_{H}$, min⁻¹ | 22.2 | 35.6 |
| $V_{Stot}$, kg | 37.5 | 3.1 |
| $R_{sys}$, kPa·ml⁻¹·min⁻¹·kg⁻¹ | 35.1 | 3.1 |
| $Q_{aorta}$, ml·min⁻¹·kg⁻¹ | 42.3 | 38.5 |
| $Q_{shunt}$, ml·min⁻¹·kg⁻¹ | 57.4 | 43.2 |
| $f_{H}$, min⁻¹ | 33.8 | 1.37 |
| $V_{Stot}$, kg | 5.4 | 0.12 |
| $R_{sys}$, kPa·ml⁻¹·min⁻¹·kg⁻¹ | 3.2 | 0.25 |
| $Q_{shunt}$, ml·min⁻¹·kg⁻¹ | 10.2 | 0.13 |

Data from previous studies is presented alongside baseline cardiac parameters from the present study for control animals (acclimated at 25°C) assessed at 25°C. $Q_{pul}$, pulmonary blood flow; $Q_{sys}$, systemic blood blow; $f_{H}$, heart rate; $V_{Stot}$, total stroke volume; $R_{sys}$, systemic resistance; $Q_{shunt}$, net cardiac shunt flow.
with previous studies on this species (14). In control animals this caused both \( Q_{\text{pu}} \) and \( Q_{\text{sys}} \) to increase; however, in cold-acclimated animals only \( Q_{\text{sys}} \) increased. This finding could relate to acclimation-induced vasculature remodeling to increase compliance in cold-acclimated animals, reducing the effect of changes in ejected \( V_{\text{tot}} \) or \( Q_{\text{total}} \) on \( P_{\text{sys}} \) (20). This idea is supported by our histological analysis of the outflow arteries, which suggests an increase in compliant elastin fibres in the cold-acclimated group. Increased vascular compliance would be able to accommodate the large increases in volume as well as reduce afterload pressure and systolic wall stress, potentially allowing systolic pressure and ejection fraction to be preserved (40). The increased elastin content would also improve recoil in the arteries, helping them to more efficiently smooth blood flow and regain their shape faster in diastole (25, 67).

The maximum \( P_{\text{arteriosum}} \) following volume load was increased in the cold-acclimated and reduced in the control group, compared with baseline values. The increased pressure response to volume suggests a decrease in ventricular chamber compliance with cold acclimation. This finding agrees with the result of our ex vivo pressure-volume relationships and ventricular connective tissue data, which suggest that the cold-acclimated ventricle was stiffer than controls, with a higher deposition of collagen in the myocardial wall. To our knowledge this is the first time pressure-volume curves have been generated in the turtle heart; however, Farrell et al. (16) used an in situ working heart preparation from slider turtles to show increased sensitivity to filling pressure following acute cold exposure, which is consistent with our findings. Data from mammals also suggest that a shift in the Frank-Starling curve due to decreased ventricular compliance can preserve systolic function and increase preload recruitable stroke work (1, 3, 23, 47). Moreover, ventricular stiffness is correlated with increased systolic pressure sensitivity to cardiac preload, and therefore, increases in central blood volume give greater increases in systolic developed pressure, even in the absence of cardiac hypertrophy as shown in these turtles (9, 20). Structural remodeling causing increased ventricular stiffness can also be associated with diastolic dysfunction and increased diastolic pressure (2, 41). It is unclear whether a reduction in cardiac compliance with associated fibrosis is beneficial or maladaptive in the turtle heart following cold acclimation. Diastolic function appears normal at low volumes as minimum \( P_{\text{arteriosum}} \) and \( P_{\text{venousum}} \) were not affected by thermal acclimation. We did not find a difference in ventricular contractility following temperature acclimation. We speculate that the lack of change is explained by thermal remodeling in the turtle heart being a physiological, rather than a pathological, response.

Maximum and minimum intraventricular pressures were similar, independent of temperature acclimation, which agrees with previous data on most reptiles (5, 35, 58). It is likely that differential pressure generation is unnecessary due to the low \( P_{\text{sys}} \) in the turtle and, therefore, low risk of pulmonary edema in the pulmonary vasculature (7, 29). In more active reptile species, such as the Burmese python (\textit{Python maurus}), the systemic side of the heart (or cavum arteriosum) generates higher pressure than the pulmonary side (68). However, in the python heart the muscular ridge between the cava is larger than that in the turtle heart, the ventricular wall surrounding the systemic side of the heart is thicker than the pulmonary side, and there is a greater degree of blood flow separation (17, 68, 70). Interestingly, although there was no change in intraventricular pressure, we did see changes in cardiac shunting patterns with an increased R-L \( Q_{\text{shunt}} \) following cold acclimation. This finding suggests that cardiac shunting is controlled entirely by peripheral resistance rather than modulating pumping pressure within the ventricle.

The effect of thermal acclimation on heart rate, stroke volume, and cardiac output. Previous studies report decreased \( f_{\text{H}} \) and \( Q_{\text{total}} \), with a corresponding increase in \( V_{\text{tot}} \) following cold acclimation (15, 62–64). However, we did not find differences in these parameters between temperature groups. Indeed, our values for these parameters in both groups better correlate to previously reported baseline levels under anesthesia at \( \sim 25^\circ\text{C} \) (Table 1) (10, 11, 13, 21, 30, 31, 36, 50). Our blood flow values are lower than that of most other studies. The basis for this difference was not clear but may relate to intraventricular pressure cannula placement, which is the main difference between this study and those previously conducted. As the animals in the present study were anesthetized and ventilated, \( f_{\text{H}} \) and \( Q_{\text{total}} \) are likely higher than if the animals were nonanesthetized and apnoeic as anesthesia blunts vagal tone on the heart and pulmonary artery (11, 50). Our findings suggest that, although cold-acclimated animals show depressed \( f_{\text{H}} \) and \( Q_{\text{total}} \) with an increased \( V_{\text{tot}} \) when studied at \( 5^\circ\text{C} \), the main driver of these changes is acute cold rather than cold acclimation per se. Indeed, Stecyk et al. (63) came to a similar conclusion in regard to \( f_{\text{H}} \) while working with spontaneously beating whole heart preparations.

Perspectives and Significance

Prolonged cold initiates profound alterations in ectotherm physiology. In the case of the freshwater turtle, acute cold triggers large depressions in metabolic rate to initiate winter hibernation/brumation and results in modifications in cardiovascular function (26). The data presented in this study builds from previous studies in freshwater turtles (15, 27, 28), indicating that cold acclimation alters cardiac shunting patterns with an increased R-L \( Q_{\text{shunt}} \), achieved through a reduction in \( R_{\text{sys}} \) and an increase in \( Q_{\text{sys}} \). Furthermore, cold acclimation increased the heart’s sensitivity to an in vivo volume load, which may be relevant during hibernation, when diving turtles have been suggested to increase \( V_{\text{tot}} \) by up to fivefold (6). Ex vivo passive filling of the ventricle revealed a reduction in ventricular compliance, which was associated with fibrosis of the myocardium. In turn, the major outflow arteries exhibited an increase in elastin content of the elastic lamellae suggesting increased outflow vessel compliance following cold acclimation. These findings suggest that cold-induced structural cardiovascular remodeling alters the hemodynamics of freshwater turtles to limit the stress of high blood preload on the heart. It is possible that these structural changes may also compensate for decreased systolic function associated with low temperatures.

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DISCLOSURES

No conflicts of interest, financial or otherwise, are declared by the author(s).

AUTHOR CONTRIBUTIONS

A.N.K. and H.A.S. conception and design of research; A.N.K. and D.A.C.I. performed experiments; A.N.K., H.A.S., and D.A.C.I. interpreted results of experiments; A.N.K. prepared manuscripts; H.A.S., and D.A.C.I. edited and revised manuscript; A.N.K., H.A.S., and D.A.C.I. approved final version of manuscript.

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