UPDATE ARTICLE

Niclosamide-loaded nanoparticles disrupt Candida biofilms and protect mice from mucosal candidiasis

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Abstract

Candida albicans biofilms are a complex multilayer community of cells that are resistant to almost all classes of antifungal drugs. The bottommost layers of biofilms experience nutrient limitation where C. albicans cells are required to respire. We previously reported that a protein Ndu1 is essential for Candida mitochondrial respiration; loss of NDU1 causes inability of C. albicans to grow on alternative carbon sources and triggers early biofilm detachment. Here, we screened a repurposed library of FDA-approved small molecule inhibitors to identify those that prevent NDU1-associated functions. We identified an antihelminthic drug, Niclosamide (NCL), which not only prevented growth on acetate, C. albicans hyphenation and early biofilm growth, but also completely disengaged fully grown biofilms of drug-resistant C. albicans and Candida auris from their growth surface. To overcome the suboptimal solubility and permeability of NCL that is well known to affect its in vivo efficacy, we developed NCL-encapsulated Eudragit EPO (an FDA-approved polymer) nanoparticles (NCL-EPO-NPs) with high niclosamide loading, which also provided long-term stability. The developed NCL-EPO-NPs completely penetrated mature biofilms and attained anti-biofilm activity at low microgram concentrations. NCL-EPO-NPs induced ROS activity in C. albicans and drastically reduced oxygen consumption rate in the fungus, similar to that seen in an NDU1 mutant. NCL-EPO-NPs also significantly abrogated mucocutaneous candidiasis by fluconazole-resistant strains of C. albicans, in mice models of oropharyngeal and vulvovaginal candidiasis. To our knowledge, this is the first study that targets biofilm detachment as a target to get rid of drug-resistant Candida biofilms and uses NPs of an FDA-approved nontoxic drug to improve biofilm penetrability and microbial killing.

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Introduction

*Candida albicans* is a part of the normal human microbiota. In individuals with compromised immunity, the fungus typically infects target organs by overgrowth or hematogenous spread from colonized sites within the body. The incidence of hematogenously disseminated candidiasis in the United States is approximately 60,000 cases per year, making *Candida* spp. one of the most frequently isolated nosocomial bloodstream pathogens [1–4], carrying unacceptably high crude and attributable mortality rates of about 40% to 60%, despite antifungal drug treatment [5,6]. Of concern is the emergence of intrinsically drug-resistant species of *Candida*, such as *Candida auris* that can be refractory to all classes of FDA-approved antifungal drugs [7].

The success of *Candida* spp. as a pathogen is predominantly due to the organism’s ability to adhere robustly to abiotic surfaces, filament, and produce biofilm infections on medical devices [8]. A biofilm is a community of microbes attached to a surface and encased in an extracellular matrix [9–11]. Due to the sheer high density of cells [12] and the ability of these cells to produce a thick extracellular matrix [11,13], cells are shielded from environmental assaults, from innate immune cells, and from killing by antifungal drugs. Studies of catheter-related *Candida* infection have unequivocally shown that retention of vascular catheters is linked to prolonged fungemia, failure of antifungal therapy, increased risk of metastatic complications, and death (with mortality rates of >40%) [14–16]. Unfortunately, in many cases, removal of catheters or implanted devices is not possible; therefore, alternative strategies to manage biofilms are needed.

Such recalcitrance of biofilm cells is not unique to fungi but also resonates throughout the bacterial biofilm setting. Antibiotics have often proven impotent against biofilms, and to date, no antibiotic has been developed for use against biofilm infections [17]. The current most promising focus to combat bacterial biofilms has been to unhang and disperse them into a population of planktonic cells that would immediately lose properties of antibiotic resistance [17–20]. Such an approach may not be easy when it comes to *Candida* biofilms considering fungal biofilms are made up of a scaffold of hyphal elements that cannot be broken easily. However, an approach that could induce early detachment of biofilms might hold promise. Indeed, biofilm dispersed cells are more susceptible to antifungal drugs than parent biofilms [21].

Biofilms experience nutrient limitations specifically within the inner layers of the community [22]. We recently reported that a conserved mitochondrial protein NDU1 is essential for *C. albicans* respiration and survival in nonfermentative conditions [23]. Interestingly, *C. albicans* NDU1 mutant strains could develop biofilms, but these biofilms detach early from their growth substrate [23]. It was determined that the glucose-starved environment within the biofilm lead to increased reactive oxygen species (ROS) accumulation and low oxygen consumption rates in NDU1 mutant, culminating to the detachment phenotype. Here, we used NDU1 as a target to screen a repurposed library of FDA-approved small molecule inhibitors (New Prestwick Chemical Library) to isolate those that could prevent *C. albicans* growth in acetate. We identified niclosamide (NCL), which has a long history of safety and efficacy as an anthelmintic drug in children and adults. When used against *Candida*, NCL treatment was found to phenocopy the defects of an NDU1 mutant.

NCL is a weakly acidic (pKₐ: 6.87) hydrophobic drug with very low solubility in water and gastrointestinal fluids and displays poor permeability and intestinal glucuronidation, which sorely limit its oral bioavailability and in vivo efficacy [24]. To overcome this drawback, we encapsulated NCL in nanoparticles (NPs) of an FDA-approved cationic polymethylmethacrylate polymer called Eudragit EPO (EPO) to enhance its bioavailability and in vivo efficacy.
Here, we elucidate that NCL can stably be encapsulated into EPO NPs with high loading due to the molecular-level interaction between cationic EPO and weakly acidic NCL. NCL-loaded EPO NPs (NCL-EPO-NPs) show long-term physicochemical and chemical stability, inhibit growth and filamentation of C. albicans as well as C. auris, prevent biofilm growth (at concentrations as low as 0.5 to 2 μg/ml), and, most importantly, disengage preformed biofilms from their growth material. Furthermore, incorporation of NCL-EPO-NPs into an in situ thermogelling formulation facilitates their intraoral delivery and shows significantly potent antifungal activity in 2 independent mouse models of mucosal infections.

This is the first study targeting the process of biofilm detachment for identification of an anti-biofilm inhibitor. Furthermore, successful repurposing of an FDA-approved inhibitor in a nanoparticulate form for treatment against C. albicans has not been described before. In summary, we have targeted a novel Candida protein (NDU1) using nanoformulation of an FDA-approved antiparasitic drug, facilitating its rapid repurposing and development as an urgently needed antifungal agent.

Results

NCL targets mitochondrial respiration and induces biofilm detachment

Using a forward genetic screening approach, we recently identified and reported on NDU1, a gene controlling C. albicans biofilm dispersal and biofilm detachment [23]. NDU1 is a mitochondrial inner membrane protein required for respiration via Complex I of the electron transport chain, is essential for growth on alternative carbon sources, and required for virulence in vivo [23]. Our work highlighted the connection between respiration and biofilm sustenance, where impaired mitochondrial respiratory activity in an NDU1 mutant leads to reduction in biofilm dispersal and early biofilm detachment. As has been well documented in the bacterial biofilm field [17–20], we postulated that targeting early biofilm detachment is a promising approach to combat biofilm-associated infections. To test this hypothesis, we used NDU1 as a target to identify small molecule inhibitors that would inhibit NDU1-associated functions and consequently trigger biofilm detachment.

C. albicans lacking NDU1 are inviable in media containing acetate (or any other nonfermentative carbon sources) but grow as robustly as the wild type (WT) in media with glucose [23]. We harnessed this unmistakable phenotype to screen a library of 1,200 repurposed FDA-approved small molecule inhibitors against a C. albicans strain overexpressing NDU1 (OE) in media containing 1% acetate. An inhibitor that could at a low concentration of 10 μM, curtail biofilm growth of OE in acetate, but not of OE or the WT in glucose was considered a "hit". This ensured the recognition of an inhibitor that only targets NDU1 and not general viability per se.

A total of 21 inhibitors were identified that prevented >50% of OE in acetate (hit rate of 1.7%; see S1 Supporting information). However, 15 out of the 21 were either disinfectants (e.g., hexachlorophene, thimerosal) or known antifungal drugs (fluconazole, tioconazole, econazole, etc.) that were inhibitory to C. albicans growth even in glucose containing medium (S1 Supporting information) and hence were discarded. We identified antimycin A, a known inhibitor of oxidative phosphorylation as a hit in acetate and not glucose, corroborating our assay that focused on identifying inhibitors of cellular respiration. However, antimycin A is considered extremely toxic and hence disregarded as a molecule of interest. Additional hits were alexidine dihydrochloride and auranofin, which we [25] and others [26] have previously shown to be attractive molecules for antifungal development, and are currently under different stages of drug development. Nevertheless, these drugs inhibited general viability rather than
respiration and were rejected for this study. Finally, we identified NCL, an antihelminthic drug, as the only inhibitor that curtailed biofilm growth of NDU1 OE strain in acetate and not glucose, thereby potentially targeting NDU1 activity, or affecting respiratory chain in a similar manner.

**Eudragit EPO (EPO) and NCL show concentration-dependent molecular interaction leading to the stabilization of NCL in the EPO matrix**

NCL suffers from major physiochemical drawbacks such as high hydrophobicity, poor permeability, and intestinal glucuronidation, which leads to poor bioavailability, thereby greatly limiting its widespread clinical applications. NPs-based drug delivery systems have the potential to solubilize hydrophobic drugs like NCL, thus improving permeability and in vivo applicability of the drug [27]. To identify the nanoformulation polymers suitable for the development of NCL NPs, we first evaluated pharmaceutically accepted anionic (polyvinyl acetate phthalate and Eudragit S100) and cationic (EPO) polymers for their ability to stabilize NCL in the polymer matrix and to facilitate the development of NCL NPs. Our simple solvent–antisolvent precipitation method involving a fixed ratio of NCL and polymers showed that only the EPO-NCL combination could form a stable dispersion. To ascertain the stabilization effect of EPO seen in our screening studies, we evaluated solid-state interaction between NCL and EPO at various ratios (1:10, 2:10, 3:10, and 4:10 w/w) using Fourier-transform infrared (FT-IR) spectroscopy and nuclear magnetic resonance (NMR) spectroscopy. Our FT-IR spectroscopic studies showed the characteristic peak for–OH and/or N–H (amide) stretching of NCL at 3,235 cm\(^{-1}\), while O–H bending and C–N stretching vibrations appeared at approximately 1,340 and 1,280 cm\(^{-1}\), respectively (Fig 1A and 1B). Interestingly, FT-IR spectra of NCL-EPO coevaporates showed disappearance of–OH and/or N–H stretching vibrations of NCL irrespective of the weight ratio (Fig 1A), whereas O–H bending and C–N stretching vibrations of NCL showed concentration-dependent red shift (Fig 1B). Additionally, peaks corresponding to dimethylamino group [28] (2,770 and 2,820 cm\(^{-1}\)) and the carboxyl group of ester (1,723 cm\(^{-1}\)) in EPO showed concentration-dependent reduction in the peak intensity along with the red shift in NCL-EPO coevaporates (Fig 1A and 1B). The changes in FTIR spectra of NCL-EPO coevaporates compared to individual components indicate the strong concentration-dependent molecular interaction between NCL and EPO. The spectral changes suggest that hydrogen donating groups in NCL (O–H and N–H) are stabilized by hydrogen accepting groups in EPO (C = O, dimethylamino) [29,30] in a concentration-dependent manner [31–33].

We further validated the molecular interaction between NCL and EPO using NMR spectroscopy. The NMR spectra of all NCL-EPO coevaporates showed disappearance of the protons corresponding to O–H and N–H functional group in NCL irrespective of the NCL:EPO ratio, whereas the protons corresponding to the tertiary amine of EPO (dimethylamino) showed a downfield shift in NCL:EPO ratios 3:10 and 4:10 and decrease in the signal peak intensity at all NCL:EPO ratios, indicating strong hydrogen bond formation between O–H/N–H group of NCL and tertiary amine of EPO [31] (Fig 1C and 1D). Additionally, NMR spectra of NCL-EPO coevaporates showed a concentration-dependent downfield shift in the signal of aromatic protons of NCL. It is likely that the cationic center and long polymeric chain of the EPO could influence the electron density of the adjacent methylene units in NCL causing the proton shifts [34]. Thus, NMR spectroscopic studies corroborated the inferences from FT-IR studies. Taken together, spectroscopic studies confirmed the ability of EPO to stabilize NCL via molecular level interaction indicating a possibility of developing EPO NPs with a potentially high concentration of NCL.

FDA approved Niclosamide nanoparticles are effective against *Candida* biofilms
Eudragit EPO allows for stable encapsulation, high loading, and long-term stability of NCL in nanoparticles

We evaluated various FDA-approved surfactants in a simple and scalable nanoprecipitation method for the development of NCL-EPO-NPs. Surfactants such as Kolliphor RH 40 (RH 40), Poloxamer 407 (P407), Vitamin E TPGS (TPGS), Kolliphor ELP (ELP), Polysorbate 20 (PS 20): Polysorbate 80 (PS80), and Kolliphor HS 15 (HS 15) were evaluated for their ability to yield NCL-EPO-NPs with lowest particle size, acceptable polydispersity index, and colloidal stability of at least 1 day (for initial screening). The size, polydispersity, and colloidal stability of NPs varied depending upon the type of surfactant used (Fig 2A). NCL-EPO-NPs stabilized
by P407 showed optimal particle size, polydispersity, and colloidal stability and were selected for further development.

Thus, we evaluated the feasibility of developing P407-stabilized EPO-NCL-NPs with higher loading of NCL. It was possible to develop P407-stabilized EPO-NCL-NPs at NCL:EPO ratios of 1:10, 2:10, 3:10, and 4:10 (Fig 2B), indicating the feasibility of developing NCL-EPO-NPs at high NCL loading. Compared to blank EPO NPs, NCL-EPO-NPs showed lower particle size and surface charge, which further confirmed the molecular interaction between NCL and EPO in the nanoparticulate form. The UV spectrophotometric analysis (S1 Fig) showed that the encapsulation efficiency of NCL was >98% in NCL-EPO-NPs irrespective of the NCL:EPO ratio used for the nanoformulation. NCL-EPO-NPs with NCL loading of 40% (%w/w compared to EPO) showed particle size of 70.2 ± 9 nm, the average polydispersity of 0.23, the average zeta potential of +4.5 mV, and excellent colloidal stability (Fig 2A and 2B). Any attempts to prepare NCL NPs without EPO immediately led to the precipitation of NCL further confirming the critical role of EPO in the stable encapsulation of NCL (Fig 2C). The transmission electron microscopy (TEM) imaging showed that EPO-NCL-NPs have spherical morphology and a reasonable correlation with the dynamic light scattering data (Fig 2D). Raw data are found in the file S1 Data.
We carried out several studies to confirm the molecular interaction between NCL and EPO at the nanoscale. First, we evaluated the fluorescence spectra of NCL solution and NCL-EPO-NPs aqueous dispersion using a spectrofluorometer. The hydroalcoholic NCL solution showed maximum emission at 406 nm, whereas NCL-EPO-NPs dispersed in water showed maximum emission at 526 nm (Fig 3A). The significant red shift and no increase in the fluorescence quantum yield observed in the case of NCL-EPO-NPs indicate strong NCL-EPO interaction and stable encapsulation of NCL at the nanoscale. Further, we freeze dried NCL-EPO-NPs and evaluated the molecular interaction of NCL and EPO in NPs using FT-IR and NMR spectroscopy. As anticipated, the FTIR spectroscopic analysis of freeze dried NCL-EPO-NPs showed the absence of–OH and–NH stretching vibrations of NCL and shifts in the C = O stretching vibration of EPO indicating the retention of molecular interaction between NCL and EPO in the NPs (Fig 3B). Interestingly, a shift in C–O stretch (ether) of P407 (1,101 cm⁻¹) was also observed in the freeze dried NCL-EPO-NPs-FD (1,090 cm⁻¹) suggesting the molecular interaction between P407 and NCL-EPO, which may further help in the stabilization of NCL-EPO NPs (S1 Fig). The changes in the NMR spectrum of freeze-dried NCL-EPO-NPs compared to pure NCL and EPO were similar to that observed in the NCL-EPO-NPs with NCL loading of 40% w/w of EPO were either used as an aqueous dispersion or freeze dried to obtain dry powder (NCL-EPO-NPs-FD) for FT-IR and NMR analysis. (A) Spectrofluorometric analysis of NCL hydroalcoholic solution (25 ppm) and aqueous dispersion of NCL-EPO-NPs (equivalent to 25 ppm NCL) showed a significant red shift in the case of NCL-EPO-NPs indicating strong molecular interaction between NCL and EPO in the NPs. (B) FT-IR spectroscopic analysis of NCL-EPO-NPs-FD showed absence of–OH and–NH stretching vibrations of NCL and shifts in the C = O stretching vibrations of EPO indicating the retention of molecular interaction between NCL and EPO in the NPs. (C) NMR spectroscopic analysis of NCL-EPO-NPs-FD showed disappearance of protons corresponding to–OH and–NH functional groups in NCL indicating retention of strong molecular interaction between NCL and EPO in the NPs. FT-IR, Fourier-transform infrared; NCL, niclosamide; NCL-EPO-NP, NCL-loaded EPO NP; NMR, nuclear magnetic resonance; NP, nanoparticle.

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coevaporates (described previously), which further confirmed the retention of strong molecular interaction between NCL and EPO in the NPs (Figs 3C and S1).

It is imperative that the nanoformulation developed after several optimization and characterization experiments maintain long-term physical (size, polydispersity index, surface charge, and pH) and chemical (NCL content) stability. The optimized P407-stabilized NCL-EPO-NPs with different NCL loading (% w/w of EPO) were evaluated for physical and chemical stability for a period of 4 weeks. NCL-EPO-NPs with NCL loading of 40% (% w/w of EPO) showed negligible changes in the particle size, polydispersity, surface charge, and pH over a period of 4 weeks (Fig 4A and 4B). The fluorescence spectra of NCL from NCL-EPO-NPs showed no to negligible changes even after 4 weeks (Fig 4C) indicating stable encapsulation and chemical stability of NCL in the NPs. The 4-week stability data for NCL-EPO-NPs with lower NCL loading, and other characteristics are included in the Supporting information (S1 Fig). Thus, we successfully developed P407-stabilized NCL-EPO-NPs with high loading of NCL that have long-term physical and chemical stability. Raw data are found in the file S1 Data.

NCL-EPO-NP display high efficacy against *C. albicans* and *C. auris* planktonic as well as biofilm growth

We first validated NCL-EPO-NP in a dose response assay against *C. albicans* planktonic yeast cells in 96-well plates, growing in media with glucose or with acetate. While NCL-EPO-NP prevented >80% growth of *C. albicans* in acetate at 1 μg/ml (3 μM), it was not effective against *C. albicans* viability in glucose (Fig 5A). Viability measured by spot testing (Fig 5B) and XTT assay (Fig 5C) provided a visual and a quantifiable measure of the outcome, respectively. These studies indicated that NCL-EPO-NP was fungicidal at 0.5 to 1 μg/ml in acetate, however ineffective in glucose. The effect of the molecule on *C. albicans* growth in glucose was also pictured by microscopy, which clearly revealed a gradual decrease in *C. albicans* proliferation over dose escalation in acetate, whereas a steady increase in growth in media with glucose (S2 Fig). Importantly, we found that while the NPs had no effect on *C. albicans* viability in glucose, it potently inhibited *C. albicans* filamentation at concentrations as low as 0.5 μg/ml (1.5 μM) (Fig 5D). Since NDU1 was used as a target to identify niclosamide, we questioned if *C. albicans* NDU1 heterozygous strain or its deletion mutant will be more susceptible to NCL-EPO-NP. Certainly, at a concentration as low as 1 μM, both *NDU1/ndu1* as well as *ndu1/ndu1* exhibited a 29.8% (±1.5%) and 34.5% (±1%) reduction in viability, respectively. This reduction in viability worsened to 63.7% (±4.4%) for the heterozygote and 75.7% (±1.4%) for the homozygote.
after treatment with 20 μg/ml of NCL-EPO-NP. Remarkably, the drug had no effect on WT NDU1/NDU1 (0% loss in viability) even at concentrations >80 μg/ml. The NCL-EPO-NP-induced haploinsufficiency of NDU1 suggests that it is required to tolerate and is a target of NCL. Raw data are found in the file S1 Data.

Hyphal growth in *C. albicans* is vital for tissue invasion. Hence, we tested if the defect in filamentation caused by NCL-EPO-NP could block damage of human umbilical vascular endothelial cells (HUVECs) by *C. albicans*. Indeed, we found that the NCL-EPO-NPs could prevent 50% damage to HUVECs at doses between 2 and 4 μg/ml of NCL. NCL itself did not significantly damage the host cells even at 8 μg/ml (S2 Fig). Raw data are found in the file S1 Data.

Considering that filamentation is also a property imperative for biofilm growth, we investigated the effect of NCL-EPO-NP on *C. albicans* biofilm formation and on preformed biofilms. Again, NCL-EPO-NP prevented *C. albicans* biofilm growth when added at the time of biofilm initiation in RPMI—a pro-filamentation media that contains glucose. Biofilm growth was interrupted at 1 μg/ml, the dose that limits hyphal growth in the fungus (Fig 6A). In fact, when fully formed biofilms were treated for 24 hours with NCL-EPO-NP, the biofilms were found to disintegrate and detach from the wells of the 96-well plate, leading to an overall decrease in biofilm biomass as measured by the XTT assay (Fig 6B and 6C). Such striking activity of a small molecule against preformed biofilms is uncommon, especially since it does not affect cell viability. Moreover, antifungal drugs have been reported to get sequestered by the biofilm ECM, which nullifies their potency. Thus, we tested the biofilm penetrability of the EPO-NPs stained with coumarin 6, which gave the NP a green color. We found that the NPs could diffuse into the compact biofilm entity (hyphae stained red with Con A) all the way to the bottom of the biofilm cells (Figs 6D and S2). Overall, our data demonstrate that NCL-EPO-NPs...
inhibit *C. albicans* hyphal growth, which has broader implications on virulence in terms of reduced invasion and biofilm growth, resulting in containment of infection and ridding of drug-resistant biofilms.

We next questioned if NCL-EPO-NP could also display similar efficacies against drug-resistant *C. albicans* isolates or against the multidrug-resistant fungus *C. auris*. Interestingly, we found that NCL-EPO-NP exhibited inhibitory activity exceeding 80% against 2 strains of *C. auris* in media containing glucose or acetate at low concentrations of 0.5 to 1 μg/ml (Fig 7A). This meant the molecule was more potent against *C. auris* than *C. albicans* in glucose in which it only prevented filamentation. In fact, similar doses also inhibited growth of *C. auris* biofilms as measured by the XTT assay (Fig 7B) and when visualized by microscopy, which showed inhibition of biofilm growth at 1 μg/ml (Fig 7C). Furthermore, the same concentration of NCL-EPO-NP was also efficacious at inhibiting >50% of biofilm growth of 2 most fluconazole-resistant *C. albicans* strains (fluconazole MIC >128 μg/ml) and *C. auris* (fluconazole MIC >512) (Fig 7D). Raw data are found in the file S1 Data.

**NCL-EPO-NP increases intracellular ROS and reduces oxygen consumption rate in *C. albicans***

NCL was identified as the drug that potentially targets a mitochondrial protein NDU1 and negatively impacts an important aspect of cellular respiration such as the ability of *C. albicans* to grow on alternative carbon sources. We further tested its effect on other key features of mitochondrial respiration such as ROS production and mitochondrial oxygen consumption rates. Presence of NCL-EPO-NP significantly increased ROS accumulation in a dose-dependent manner, with an 11% increase at 1 μg/ml, 32% increase at 4 μg/ml and 16 μg/ml, and approximately 70% elevation at 64 μg/ml (Figs 7E and S2). The fact that cells were

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**Fig 6. NCL-EPO-NP abrogate *C. albicans* biofilm growth.** (A) Addition of NCL-EPO-NP at the beginning of *C. albicans* biofilm induction (96-well flat well microtiter plates) arrested biofilm growth at 1 μg/ml. (B) NCL-EPO-NP added on to preformed biofilms induced biofilm detachment at 2 μg/ml, which was visualized microscopically. Scale bar for 2X mag is 500 μm, and for 10X is 100 μm. (C) The effect of the NP on preformed biofilms was quantified by XTT assay, which revealed a >50% reduction in biofilm metabolic activity starting at 2 μg/ml. (D) Coumarin-tagged NCL-EPO-NP (green) could efficiently penetrate the concanavalin-stained *C. albicans* biofilm (red), as seen by the yellow-stained particles (green+red overlap). Raw data are found in the file S1 Data. NCL-EPO-NP, NCL-loaded EPO NP.

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hypersusceptible to NCL-EPO-NP in acetate indicated a faulty electron transport chain (ETC) activity [23,35]. To test this hypothesis, we carried out Seahorse assays to test the respiratory prowess of *C. albicans* in Dulbecco’s Modified Eagle Medium (DMEM) without glucose and with NCL. The cells presented a significant decrease in respiratory capacity with increasing doses of the NCL-EPO-NP. The oxygen consumption rate of cells fell below 50% between 0.5 and 1 μg/ml and reduced to >90% by 2 μg/ml (Figs 7F and S3), thus corroborating the findings of NCL MIC in media lacking glucose (Fig 5A–5C). Together, these results indicate that NCL-EPO-NP target mitochondrial respiration by interfering with the ETC.

**NCL-EPO-NP protects mice from mucosal infections**

The pronounced in vitro efficacy of NCL-EPO-NP against *C. albicans* filamentation, invasion, and biofilm growth encouraged us to test this molecule in vivo. To facilitate this, we developed a P407-based in situ gelling formulation containing NCL-EPO-NPs. Following a strategy previously reported by us [36,37], NCL-EPO-NPs were incorporated in an in situ gelling formulation composed of 20% w/v P407 and 1% w/v Poloxamer 188 (S3 Fig). Incorporation of the NCL-EPO-NP in a gel form allowed us to facilitate their delivery directly into mucosal organs of mice.

We evaluated NCL-EPO-NP first in the established mouse model of oropharyngeal candidiasis (OPC) [38,39]. Mice pretreated with corticosteroids were infected sublingually with *C. albicans*. After allowing the infection to establish for 2 days, cohorts of mice were treated...
with fluconazole or NCL-EPO-NP gel. Fluconazole was administered systemically, whereas the drug-containing gel was introduced into the mouth of the mice. Antifungal activity was assessed by measuring residual colony-forming units (CFUs) persisting on the tongue after completing 4 days of therapy. NCL-EPO-NP gel treatment decreased fungal burden by almost one log, compared to untreated mice and mice treated with placebo gel without NCL (Fig 8A).

We further investigated the potency of NCL on OPC infection induced by a fluconazole-resistant clinical isolate of *C. albicans* (fluconazole MIC > 128 μg/ml). Again, NCL displayed impressive protection lowering the fungal burden in the oral mucosa by 10-fold versus fluconazole, which had no effect on curtailing the infection, as expected (Fig 8B). Microscopic analysis of tongue tissue sections stained with PAS revealed *C. albicans* infection of the superficial epithelial layer similar to pseudomembranous OPC in humans [38]. While placebo gel-treated and fluconazole-treated mice tongues had widespread infection with abundant tissue penetrating hyphae, NCL-treated tongues on the other hand displayed comparatively limited lesions, with the infection sites containing a strikingly large numbers of yeasts and pseudohyphae (2X and 10X in Fig 8C, 40X in S3 Fig). To validate that NCL-EPO-NP is indeed able to repeal mucosal candidiasis, we additionally tested it independently in a mouse model of vulvovaginal candidiasis. Here too we found that NCL-EPO-NP dose of 20 μg almost completely abrogated mice vaginal infections from the fluconazole-resistant *C. albicans* (S3 Fig). Fungal burden in NCL-treated mice was at least 1.5 log lower than placebo- or fluconazole-treated mice. Overall, these in vivo studies serve as a testimony to the

Fig 8. NCL-EPO-NP is efficacious against OPC. (A) Steroid-treated outbred CD1 mice were infected in their oral mucosa with *C. albicans* SC5314 and were treated intraorally with NCL-EPO-NP gels at 200 μg per dose, twice/day for 4 days. The mice were also treated similarly with gels without NCL as a placebo control and intraperitoneally with fluconazole on days 3 and 4. Mice killed at day 5 postinfection (7 mice per arm) were monitored for fungal CFU in their tongue and presented as log CFU/gm of tissue. (B) Efficacy of NCL-EPO-NP in preventing OPC was also seen during infection by a fluconazole-resistant strain of *C. albicans*. (C) The tongues infected with a fluconazole-resistant strain and treated with placebo, NCL-EPO-NP, or fluconazole were sectioned for histology, stained with PAS, and microscopically visualized at 2X or 10X magnification. Scale bar for upper panel 500 μm, and lower panel 100 μm. Raw data are found in the file S1 Data. CFU, colony-forming unit; NCL, niclosamide; NCL-EPO-NP, NCL-loaded EPO NP; OPC, oropharyngeal candidiasis; PAS, periodic acid–Schiff.

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fact that the anti-hyphae/anti-biofilm activity of NCL-EPO-NP seen in vitro is also manifested in vivo thereby proving efficacious in prevention of mucosal candidiasis. Raw data are found in the file S1 Data.

**Discussion**

Biofilms display physical gradients of nutrients and gases due to metabolic activity and solute diffusion [40]. The sheer density of cells in an exponentially growing biofilm and the secretion of extrapolymeric substances restrict nutrient diffusion into the innermost layers. This creates a stressful environment especially for the “originator” cells that lay the foundation of biofilm growth on a substrate. Indeed, it is known that *C. albicans* biofilms provide a hypoxic microenvironment, where oxygen concentration decreases steadily from the top to the bottom layers [41]. This happens to such a prominent extent, that deeper layers of *C. albicans* biofilms can sustain growth of obligate anaerobic bacteria. Certainly, the respiratory capacity of *C. albicans* becomes undeniably necessary during this time, with genes associated with mitochondrial respiration up-regulated significantly [41]. In fact, the respiratory electron transport chain activity also helps *C. albicans* survive in a glucose-deficient environment and could prove imperative for adaptation of the fungus to nutrient-poor environment in the biofilm core [35].

We recently published that NDU1, a *C. albicans* mitochondrial protein, is required for the assembly and activity of the NADH ubiquinone oxidoreductase Complex I (CI) of the respiratory ETC [23]. Absence of NDU1 blocked oxygen uptake, increased ROS accumulation, caused mitochondrial depolarization, and prevented *C. albicans* growth on several alternative carbon sources. This phenotype resulted in hypersusceptibility of the fungus to innate immune cells and rendered *Candida* avirulent in a disseminated mouse model. Interestingly, while the NDU1 mutant could develop a robust biofilm, these biofilms were fragile and detached easily from their growth substrate [23]. Although the exact reason of why NDU1 loss causes biofilm detachment is not known, it is plausible that its absence disallows *C. albicans* to adapt to the hypoxic and nutrient-poor environment rampant in the bottommost biofilm layers. We utilized these phenotypes to identify inhibitors of NDU1 and inducers of early biofilm detachment.

NDU1 mutant grows as adeptly as the WT in media containing glucose but is completely inviable in acetate as the sole source of carbon. We created a strain of *C. albicans* that overexpressed NDU1 (OE), which can grow both on glucose and acetate. From screening a repurposed library of approximately 1,200 FDA-approved inhibitors against this strain, we identified NCL, which at a low concentration of 10 μM, prevented growth of OE in acetate by 50%, but not in glucose. This indicated that NDU1 could be the target of NCL. It also meant that NCL could be a valuable antifungal molecule considering that the host environment is almost devoid of glucose. Host niches, e.g., bloodstream and tissues, only have approximately 0.05% to 0.1% glucose [42]. FDA-approved molecules such as NCL that target respiratory activity of *Candida*, which is needed to survive in vivo, could be a promising new class of antifungals.

NCL is an anthelmintic indicated in the treatment of tapeworm infections in humans. It is listed on the WHO’s list of essential medicines (file:///C:/Users/puppuluri/Downloads/WHO-MVP-EMP-IAU-2019.06-eng.pdf). It has impressive anticancer activity (NCI-lead Phase I and II clinical trials against prostate and colon cancer) and has shown remarkable promise for its broad-spectrum antiviral effect, including on Severe Acute Respiratory Syndrome Coronavirus 2 (SARS-CoV-2) [43–45]. Unfortunately, NCL is minimally absorbed from the gastrointestinal tract—neither the drug nor its metabolites have been recovered from the blood or urine [29]. The poor systemic bioavailability of NCL is because of its limited
aqueous solubility of only 0.23 μg/ml. We reckoned that the best use of NCL as an antifungal drug will only be possible if its solubility and absorption characteristics are improved, and the drug can be developed in a way that does not require high doses to enable an antifungal outcome.

One strategy for improving NCM drug solubility has been synthesis of water-soluble analogs [46,47]. However, these new derivatives require comprehensive preclinical/clinical studies to confirm their efficacy and safety and will face several regulatory hurdles prior to approval. An alternate approach is to transform the formulation of this FDA-approved drug by using into clinically viable nanformulations comprised of pharmacologically acceptable excipients to improve its delivery. We exploited a formulation-based approach using an FDA-approved cationic polymethacrylate polymer Eudragit EPO (EPO), for which the pharmacological and toxicological profiles are already known (https://www.fda.gov/media/107564/download). EPO is used in pharmaceutical products as a coating material to achieve taste masking, moisture protection, modified drug release, and for colon targeting [48–51]. Additionally, EPO, in the form of solid dispersion or NPs, has been used to improve solubility and oral bioavailability of various hydrophobic drugs including weakly acidic drugs [52–55].

We and others have previously shown that encapsulation of a weakly acidic and poorly bioavailable anti-inflammatory drug called meloxicam in EPO NPs can improve its efficacy on oral administration with a concomitant reduction in its side effects [31,56]. Given that NCL is weakly acidic and is as hydrophobic as meloxicam, we hypothesized that cationic EPO could encapsulate and stabilize NCL in the NPs via electrostatic interactions. Our preliminary screening involving anionic carboxylic acid terminated polymers such as Eudragit S100, PVAP, and cationic EPO confirmed our hypothesis. Polymeric dispersions prepared with Eudragit S100 or PVAP showed rapid precipitation of NCL indicating insufficient interaction and encapsulation of NCL with the anionic polymers. On the contrary, EPO-NCL dispersion showed significant enhancement in color (yellow color) and no signs of NCL precipitation indicating strong interaction and encapsulation of NCL with the cationic polymers. Our preliminary screening involving anionic carboxylic acid terminated polymers such as Eudragit S100, PVAP, and cationic EPO confirmed our hypothesis. Polymeric dispersions prepared with Eudragit S100 or PVAP showed rapid precipitation of NCL indicating insufficient interaction and encapsulation of NCL with the anionic polymers. On the contrary, EPO-NCL dispersion showed significant enhancement in color (yellow color) and no signs of NCL precipitation indicating strong interaction and encapsulation of NCL. Our FT-IR and NMR spectroscopic studies confirmed the strong interaction between NCL and EPO at various ratios and corroborated the color enhancement and higher stability observed for NCL-EPO dispersions. While EPO and NCL dispersion showed signs of stability, in order to develop NPs with long-term stability, we evaluated various FDA-approved nonionic surfactants with different chemical structures and HLB values to prepare NCL-EPO-NPs with lowest size and acceptable homogeneity. While nonionic surfactants such as Kolliphor RH40, Vitamin E TPGS, and Kolliphor P407 (P407) yielded NCL-EPO-NPs with similar size, we selected P407 as a stabilizer due to its ability to yield higher stability of NCL-EPO-NPs in the initial screening and its capability to enhance penetration and delivery of NPs to the mucosal surfaces [55,57,58].

The amount of drug loaded into the NPs significantly impacts the total amount of NPs required for the intended therapeutic effect. Our studies on the loading of NCL into NCL-EPO-NPs revealed a possibility of significantly higher NCL loading into NCL-EPO-NPs (NCL: EPO ratio 4:10 or 40% w/w of EPO) without compromising its size and colloidal stability. Interestingly, hitherto reported NCL nanoformulations involving use of materials such as natural polysaccharides (chitosan and xylan), solid lipids, inorganic materials such as mesoporous silica and halloysite, and biodegradable polymers such as polylactide-co-glycolide (PLGA) to load NCL were unable to achieve NCL loading >10%, and none of these reports evaluated long-term colloidal stability of NCL nanoformulations [59–64]. Remarkably, our investigation demonstrated, for the first time, high NCL loading in NPs due to strong interaction between NCL and EPO and at least 4 weeks of colloidal stability of NCL-EPO-NP.

The effect of NCL parent drug against Candida has previously been studied in vitro [65], against planktonic and biofilm conditions. While that study and ours concur that NCL is not...
fungicidal to \textit{C. albicans} in media containing glucose, we showed that encapsulation in NPs significantly decreases \textit{C. albicans} growth and filamentation in glucose containing media (Figs. 5A, 5D and S4). NCL-EPO-NPs prevented \textgreater 80\% hyphal growth at a striking 6- to 30-fold lower concentrations than the parent drug alone in RPMI, a hyphal-promoting media ([65] and S4 Fig). These low doses of the drug-loaded NPs could also prevent \textit{C. albicans} invasion of HUVECs at a conspicuous 10- to 15-fold better efficacy than the generic drug alone. Such enhanced anti-invasive activity can be attributed to the complete aqueous solubility, better absorption, and thus improved distribution of NCL due to EPO-NP encapsulation.

Indeed, prevention of germination and subsequent hyphal formation by NCL-EPO-NPs contributed to its enhanced anti-biofilm activity. Noteworthy was the finding that NCL-EPO-NPs (but not parent NCL; S4 Fig) could disengage developing biofilms early in their development and penetrate mature biofilms and detach them from their growth surface. Promisingly, NCL-EPO-NPs were not sequestered by the biofilm matrix, a process notoriously known for failure of most antifungal drugs against biofilms [66]. A previous report suggested that interaction between cationic EPO and anionic fluoroquinolones such as ofloxacin could potentiate the permeation and antibacterial activity of ofloxacin by modulation of the electronegative membrane potential of the bacteria leading to alterations in the outer membrane [67]. Given the fact that \textit{C. albicans} exhibits negative membrane potential [68], the enhancement of antifungal activity of NCL via encapsulation into EPO NPs could be a combined effect of nanoencapsulation and modulation of the overall negative membrane potential of the \textit{Candida} biofilms.

Bottommost layers of biofilms are hypoxic and nutrient-starved, subjecting the cells present in the deeper layers to stress, which is combatable by up-regulating the fungus's respiratory machinery. Premature detachment of fully formed biofilms due to NCL-EPO-NP treatment could prospectively be due to loss of viability at the bottommost nutritionally disadvantaged layers of the biofilm, coupled with an early loss of adhesion to substrate due to alterations in the cell wall architecture. We have previously elucidated that loss of NDU1 has a direct impact on \textit{C. albicans} cell wall remodeling and cell membrane integrity (reduction in chitin, cell surface mannan, and decrease in ergosterol content) making it susceptible to cell wall and cell membrane perturbing agents [23]. Biofilm disintegration has been considered the gold standard for ridding bacterial biofilm-mediated infections [19,69]. Truly, prevention of \textit{C. albicans} biofilms or disintegration of the microbial community early in their development could prove a stellar strategy rendering dissociated cells more susceptible to antifungal drugs [21,69]. The current study is the first to identify a molecule capable of inducing \textit{C. albicans} biofilm detachment.

In an alternative carbon source like acetate, NCL-EPO-NPs were found fungicidal. \textit{C. albicans} can tolerate loss of mitochondrial activity in the presence of glucose, but not in its absence [35]. Thus, a drug that targets NDU1, an inner mitochondrial membrane protein necessary for electron transport, is expected to be potent under conditions of stress created by the absence of the preferred carbon source. Indeed, NCL-EPO-NPs displayed many of the same phenotypic/biochemical defects as seen in an NDU1 mutant (ROS accumulation, decrease in OCR). Interestingly, unlike \textit{C. albicans}, NCL-EPO-NPs killing activity of \textit{C. auris} was not dependent on carbon source preference. NCL-EPO-NPs prevented planktonic growth of \textit{C. auris} both in glucose and acetate containing media. \textit{C. auris} metabolism favors respiration even in the presence of glucose, as evidenced by enrichment in glycolytic and sugar transporter gene expression during yeast growth and TCA cycle protein enrichment compared to \textit{C. albicans} [70,71]. Respiratory metabolism enhances ATP production and can reduce oxidative stress, also promoting in vivo fitness and fluconazole resistance [72]. Thus, NCL-EPO-NP that targets cellular
respiration proved lethal to *C. auris* and is poised to be an attractive novel antifungal drug targeting infections caused by this MDR fungus.

The pronounced in vitro efficacy of NCL-EPO-NPs against *C. albicans* filamentation, invasion, and biofilm growth encouraged us to test this molecule in vivo. Previous characterization of NCL pharmacokinetics have revealed poor absorption, which challenges the drug’s efficacy by reducing the dose that reaches the target tissue, precluding its testing in mouse models of bloodstream *Candida* infection [73]. To overcome this limitation and investigate its antifungal potential in vivo, we tested NCL-EPO-NP in 2 different mucosal models of candidiasis. For uniform delivery of NCL-EPO-NP on intraoral and intravaginal administration, we incorporated NCL-EPO-NP into our previously reported thermosensitive gel composition containing 20% P407 and 1% Poloxamer 188. We and others have demonstrated that thermosensitive P407 hydrogels can be effectively used for the intraoral and intravaginal application of NPs without affecting their inherent properties and release [36,37,74,75]. Additionally, we have previously shown that NPs stabilized with P407 show significant enhancement in mucosal transport in vivo leading to improved efficacy [57,58,76]. Finally, studies have also shown that Poloxamer 407 thermosensitive hydrogel can also interfere with the formation of microbial biofilms [75,77,78]. Taken together, usage of mucus-penetrating P407 as a stabilizer for EPO-NCL-NPs and P407 thermosensitive gel to deliver NCL-EPO-NPs was deemed advantageous for improving outcome of in vivo studies. In both OPC [38] as well as the VVC models [79], NCL-EPO-NP significantly prevented mucosal fungal burden. This was unmistakably evident by a reduction in oral thrush on the tongue and oral palette of treated mice. The drug prevented *C. albicans* filamentation in vivo: Histology revealed a remarkable presence of abundant yeast cells in NCL-EPO-NP-treated tongue, while the mice treated with placebo or fluconazole displayed a heavy load of filamentous cells. This clearly demonstrated that the efficacy of NCL-EPO-NP in vitro against filamentation and biofilm growth could also be deciphered in vivo in 2 biofilm models of mucosal candidiasis.

In summary, we have targeted the respiratory function of *C. albicans* NDU1 to identify an FDA-approved antiparasitic drug NCL with antivirulence activity. Additionally, we used an FDA-approved EPO polymer to encapsulate NCL and improve its aqueous solubility, antifungal potency, biofilm penetrability, and antifungal activity in vivo. This is the first report on the nanoformulation comprised of FDA-approved components that can detach *Candida* biofilms in vitro and prevent biofilm infections in vivo. Strategies using FDA-approved molecules and materials can undercut the time required for antifungal development and can enhance antimicrobial activity by improving the physiochemical properties of pharmacologically difficult molecules.

**Materials and methods**

**Strains, media, and culture conditions**

The following fungal strains were used in this study: *C. albicans* strain SC5314, which is a clinical isolate recovered from a patient with generalized candidiasis [80], and 2 clinical isolates of *Candida* spp. received from the Fungus Testing Laboratory at the University of Texas Health Science Center at San Antonio—fluconazole-resistant *C. albicans* CA6 and CA10. The 2 *C. auris* isolates CAU-03 and CAU-09 were a kind gift from Shawn Lockhart, Centers for Disease Control and Prevention (CDC). All cultures were maintained by subculture on yeast peptone dextrose (YPD) medium at 37˚C, and stocks of these cultures were stored in 20% glycerol at −80˚C.
Materials

NCL was purchased from Biosynth-Carbosynth (San Diego, CA). Eudragit EPO and Eudragit S100 (Evonik Corporation, Los Angeles, CA), polyvinylacetate phthalate (Colorcon, West Point, PA), and Vitamin E TPGS NF grade (Antares Health Products, Jonesborough, TN) were received as gift samples. Poloxamer 407 (Kolliphor P407), Poloxamer 188 (Kolliphor P188), Kolliphor ELP, Kolliphor RH40, Kolliphor HS15, Kolliphor PS80, and Kolliphor PS20 were obtained as gift samples from BASF ( Florham Park, NJ). Acetone (AR Grade), scintillation vials (7 ml and 20 ml), and Coumarin C6 were purchased from VWR International (Radnor, PA). Ultrapure distilled water was used for all experiments.

HTS

Screening was performed at the Molecular Screening Shared Resource facility at the University of California, Los Angeles. A total of $5 \times 10^6$ C. albicans yeast cells/ml was suspended in yeast nitrogen base containing 2% acetate as an alternative carbon source and plated (50 μL) into individual 384-well plates using an automated Multidrop 384 system (Thermo Labsystems). The New Prestwick Chemical Library consisting of 1,233 drugs was used to pin 1 compound per well at 10 μM final concentration, using a Biomek FX liquid handler. Twenty-four hours later, the plates were scanned with a Flex Station II 384-well plate reader (Molecular Devices) to measure turbidity (OD600) of the wells. Molecules displaying > 50% reduction in turbidity compared to control nondrug-treated wells (MIC50) were considered primary “hits.”

Preliminary studies to assess stabilization potential of Eudragit EPO

A preliminary study was carried out to evaluate the potential of Eudragit EPO (cationic polymethacrylate), polyvinylacetate phthalate (PVAP; anionic polycarboxylate), and Eudragit S100 (anionic polymethacrylate) to stabilize weakly acidic NCL. Briefly, NCL (10 mg) and Eudragit EPO/PVAP/Eudragit S100 (100 mg) were transferred to a 20-ml scintillation vial, and the mixture was dissolved in 10 ml of acetone to obtain a uniform solution. Ultrapure water (10 ml) was transferred to a 50-ml clean and dry beaker, and the beaker was placed on a magnetic stirrer. Organic solution containing NCL, and the polymer was added dropwise to the aqueous solution and the mixture was stirred at 600 rpm in a fume hood for 3 hours to evaporate acetone. The resultant dispersion was observed for signs of precipitation over a period of time.

Evaluation of concentration-dependent molecular interaction between EPO and NCL using Fourier-transform infrared (FT-IR) spectroscopy and nuclear magnetic resonance (NMR) spectroscopy

For the spectroscopic studies, NCL and EPO in different weight ratios (% w/w NCL: EPO = 1:10, 2:10, 3:10, and 4:10) were weighed and transferred to a scintillation vial. The mixture was dissolved in acetone to obtain a uniform solution. Acetone was evaporated using a rotary evaporator (Scilogex, Rocky Hill, CT) to obtain a solid dispersion of NCL and EPO. The solid dispersion was further dried overnight using a vacuum oven (Fisher Scientific, Waltham, MA). The NCL-EPO solid dispersions, EPO, and NCL were evaluated using the FTIR spectrometer (Nicolet iS10, Thermo Scientific, Waltham, MA) equipped with a diamond attenuated total reflection unit. The FTIR spectra were obtained in the transmission mode from 4,000 to 500 cm$^{-1}$. The 1H NMR spectra of NCL-EPO solid dispersions, EPO, and NCL were obtained using a Bruker Avance Digital 400 MHz NMR spectrometer (Bruker, Billerica, MA) coupled to a BACS 1 automatic sample changer. The spectrometer is equipped with a 5-mm PABBO BB- 1H/D Z-GRD probe. The spectra of the samples were recorded in (400 μl)
Development and characterization of NCL-loaded Eudragit EPO nanoparticles (NCL-EPO-NPs): Screening of surfactants for their ability to form NCL-EPO-NPs

Various FDA-approved surfactants such as Poloxamer 407 (P407), Kolliphor ELP (ELP), Kolliphor RH40 (RH40), Kolliphor HS15 (HS15), Kolliphor PS80 (PS80), Kolliphor PS20 (PS20), and Vitamin E TPGS (TPGS) were screened for the development of NCL-EPO-NPs. Briefly, Eudragit EPO (50 mg), NCL (5 mg), and surfactant (200 mg) were transferred to a 20-mL scintillation vial, and the contents were completely dissolved in 10 mL acetone by vortexing (organic phase). The aqueous phase consisting of 10 mL ultrapure water was transferred to a clean 50-mL beaker. The beaker containing water was placed on a multipoint magnetic stirrer (IKA Works) and the stirrer was set at 600 rpm. The organic phase was slowly added to the aqueous phase to avoid any splashing and to allow the formation of NPs. The stirring was continued for at least 3 hours in a fume hood to allow for complete evaporation of the organic solvent. The NP synthesis experiment was carried out in triplicate. The size and polydispersity index of various NCL-EPO-NPs were evaluated using Litesizer 500 particle analyzer (Anton-Paar USA, Torrance, CA). The surfactant that yielded NCL-EPO-NPs with the lowest size and polydispersity index was selected for further experiments.

Preparation of NCL-EPO-NPs with different NCL loading and their characterization

Previously carried out EPO-NCL molecular interaction studies formed the basis for the preparation of NCL-EPO-NPs with different NCL loading. Briefly, NCL (10, 20, 30, or 40 mg), EPO (100 mg), and P407 (400 mg) were transferred to a 20-mL scintillation vial and dissolved in 10 mL of acetone to obtain a homogenous organic phase. The aqueous phase consisting of 10 mL ultrapure water was transferred to a clean 50-mL beaker. The remaining procedure for the preparation of NCL-EPO-NPs was similar to that described in the earlier section. The size, polydispersity index, and zeta potential of various NCL-EPO-NPs were evaluated using Litesizer 500 particle analyzer (Anton-Paar USA, Torrance, CA). The NP synthesis experiment was carried out in triplicate. For TEM imaging, NCL-EPO-NPs with NCL loading of 40% wt/w EPO were selected. Briefly, samples were applied to glow-discharged 200 mesh carbon-coated Formvar-coated copper grids and allowed to dry. Grids were viewed on a Hitachi HT7700 TEM at 100 kV and photographed with an AMT XR-41B 2k × 2k CCD camera.

Determination of the encapsulation efficiency of NCL in NCL-EPO-NPs

NCL-EPO-NPs dispersion (0.5 mL) was transferred to the Amicon Ultra-0.5 device (3 kDa membrane; Fisher Scientific, Waltham, MA). The Amicon-Ultra centrifugal filter containing NCL-EPO-NPs was centrifuged for 15 minutes at 14,000 rpm (Thermo Scientific, Legend Micro 17R centrifuge). The filtrate was then diluted 10-fold with methanol, and NCL concentration in the filtrate was measured at 340 nm using a UV-Vis spectrophotometer. The % encapsulation efficiency (EE) was calculated by the following equation:

\[
\text{%EE} = \left( \frac{D_{\text{initial}} - D_{\text{free}}}{D_{\text{initial}}} \right) \times 100
\]
where “D_{initial}” is the amount of NCL/mL of EPO-NCL-NPs dispersion and D_{free} is the amount of NCL/mL of the filtrate obtained by the centrifugation of NCL-EPO-NPs.

**UV-Vis spectrophotometric determination of NCL from NCL-EPO-NPs**

Briefly, NCL (10 mg) and EPO (25 mg) were transferred to a 100-ml volumetric flask, and the contents were dissolved in 100 ml methanol to obtain a stock solution of NCL (NCL concentration 100 μg/ml). The stock solution was suitably diluted with methanol:water (99:1) to obtain various NCL concentrations (2, 2.5, 5, 7.5, 10, 15, and 20 μg/ml). The absorbance of solutions containing various NCL concentration was measured at 340 nm using Agilent Carey 60 UV-Vis Spectrophotometer. NCL calibration curve was obtained \((n = 3)\) by plotting a graph of NCL absorbance Vs NCL concentration. For the determination of NCL content from NCL-EPO-NPs, the NPs were diluted 100- to 1,000-fold with methanol to obtain NCL concentration with the range established by NCL calibration curve and the absorbance of the NCL was measured at 340 nm.

**Evaluation of molecular interaction between NCL and EPO in NCL-EPO-NPs using fluorescence spectroscopy, FT-IR, and 1H-NMR**

Fluorescence spectroscopy was used to determine the molecular interaction between EPO and NCL in NCL-EPO-NPs dispersion. Briefly, NCL-EPO-NPs with NCL loading of 40% w/w EPO were diluted with water to obtain a solution with NCL concentration of 25 μg/ml. NCL hydroalcoholic solution (NCL concentration: 25 μg/ml) was used as a control. The fluorescence spectra of NCL from NCL-EPO-NPs dispersion and control NCL solution was evaluated using Shimadzu RF 5301 Spectrofluorometer using an excitation wavelength of 310 nm for NCL solution and 330 nm for NCL-EPO-NPs. For the NCL solution, the excitation wavelength of 310 nm was used to minimize Raman scattering associated with the solvent that interfered with the fluorescence analysis. For FT-IR and NMR characterization, NCL-EPO-NPs were freeze dried. Briefly, NCL-EPO-NPs containing NCL loading of 40% w/w were transferred to a scintillation vial, and the contents in the vial were flash frozen using liquid nitrogen. The frozen vial was transferred to a freeze drying flask, and the freeze drying flask containing NCL-EPO-NPs samples were loaded on the Labconco FreeZone 12 Plus freeze dryer preset at −80˚C temperature and <0.12 mb pressure. After 24 hours of lyophilization, the samples were removed from the freeze dryer, and the vial containing freeze dried NCL-EPO-NPs were stored in a vacuum desiccator until further use. The freeze-dried NCL-EPO-NPs were evaluated using FT-IR and NMR to ascertain molecular interaction between NCL and EPO in the NPs.

**Evaluation of long-term physical and chemical stability of EPO-NCL-NPs**

The optimized EPO-NCL-NPs containing different loading of NCL were evaluated for the 4-week long physical stability (size, polydispersity index, zeta potential, and pH), whereas NCL-EPO-NPs containing 40% w/w NCL was evaluated for 4-week long chemical stability using fluorescence spectrophotometer.

**Preparation of Coumarin-6 encapsulated polymeric NPs**

Briefly, Eudragit EPO (100 mg) and Kolliphor P407 (400 mg) were transferred to a 20-mL scintillation vial along with 9.95 ml of acetone. The contents in the scintillation vial were vigorously vortexed to obtain a clear solution (organic phase). Coumarin-6 (Acros, Organics) was dissolved in acetone at a concentration of 2 mg/mL and added to the organic phase containing
polymers to obtain a final concentration of 0.01 mg/mL. The polymeric NPs were prepared as described earlier. The unencapsulated Coumarin-6 in the NPs was removed using Amicon Ultra-0.5 Centrifugal Filter Devices (Amicon Ultra 10K device). Briefly, NP dispersion (0.5 mL) was transferred to the Amicon-Ultra-0.5 device and centrifuged for 15 minutes at 14,000 rpm (Thermo Scientific, Legend Micro 17R centrifuge). The NPs were washed twice with ultrapure distilled water to get rid of free Coumarin-6. The filtrate was discarded and the concentrated Coumarin-6 encapsulated polymeric NPs (approximately 100 μL) were collected in a separate tube by inverting and centrifuging the Amicon Ultra filter for 2 minutes at 1,000 rpm. The concentrated NPs were then diluted to their original volume by adding approximately 400 μL of distilled water; the tube was covered with aluminum foil and stored until further use.

Development of NCL-loaded Eudragit EPO nanoparticles (NCL-EPO-NPs) thermosensitive gel

Briefly, 10 mL of blank EPO-NPs were taken in a 20-mL scintillation vial. Kolliphor P407 (20% w/v) and Kolliphor 188 (1% w/v) were added into it and vortexed. The vial was kept in the refrigerator (4˚C) for 3 hours to ensure total dissolution of surfactants. The same procedure was performed to obtain NCL-EPO-NPs thermosensitive gel of the optimized batch.

Dose–response assays

Dose–response assay of NCL-EPO-NP against planktonically grown fungi was performed in agreement with the CLSI M27-A3 (for yeast) reference standards for antifungal susceptibility testing [81]. Each drug was used in the concentration range of 0.6 μg/ml to 64 μg/ml, and the MIC of NCL-EPO-NP in media containing 2% acetate was compared to media containing 2% glucose. Inhibition of planktonic growth or filamentation due to drug treatment was also visualized and imaged using bright-field microscopy.

Biofilm growth and drug susceptibility testing

Biofilms of Candida spp. were developed in 96-well microtiter plates, and susceptibility of the biofilm cells to NCL-EPO-NP was determined as described previously [82]. Biofilms were initiated in either the presence or absence of the drugs, or the drugs were tested on 48-hour pre-formed biofilms. Inhibition of biofilm growth was measured by a standard colorimetric assay (XTT) that measures metabolic activity of the biofilm cells [82]. Absorbance at 490 nm was measured using an automated plate reader. Biofilm disruption by the NCL-EPO-NP were also visualized by bright field microscopy. C. albicans 48-hour mature biofilms were also treated with 2 μg/ml coumarin-6 encapsulated NCL-EPO-NP for 24 hours. Biofilms were additionally stained with 25 μg/ml concanavalin A to visualize the cells in red. Confocal microscopy with z-stacking feature was performed, and images were collected at 2 wavelengths, 488 nm (GFP) and 594 nm (ConA) as published previously [83].

ROS measurement

Intracellular ROS production was detected by staining cells with 5 μM MitoSOX Red (Life Technologies, Frederick, Maryland, USA) in DMSO. Cells from 25-ml cultures grown for 6 hours at 30˚C in the presence and absence of NCL-EPO-NP in YPD medium were collected and washed twice with PBS. The pellets were suspended to 1 × 10^6 cells in 1 ml of PBS and treated with or without MitoSOX Red for 45 minutes at 30˚C in the dark. Cell fluorescence in the presence of DMSO alone was used to verify that background fluorescence was similar per
strain. Cells from each MitoSOX-treated sample were collected and washed twice with PBS after staining, and mean fluorescence for ROS was quantified.

**Oxygen consumption rate assay**

OCR were measured under a Seahorse instrument (Seahorse Bioscience, Massachusetts, USA) according to the manufacturer’s instructions. Cells were plated in poly-d-lysine-coated XF96 microplates at a density of $5 \times 10^4$ cells/well in 100 μL volume of unsupplemented DMEM (no glucose) with or without NCL-EPO-NP. Samples were run with 3 technical replicates per condition. The plates were centrifuged at 1,000 rpm for 4 minutes without use of the centrifuge break. After centrifugation, plate was incubated for 5 minutes before being loaded into a Seahorse XF96 Extracellular Flux Analyzer (Agilent). Basal respiration was measured over 6 hours with 36 ten-minute protocol cycles including a 3-minute mix, 4-minute wait, and 3-minute measurement. After 6 hours, the Complex I and Complex III electron transport chain inhibitors rotenone and antimycin A were injected from Ports A and B at a final concentration of 5 μM to determine nonmitochondrial respiration. Data analysis included subtraction of nonmitochondrial respiration from basal respiration measurements before averaging the last 4 basal measurements.

**Mammalian cell damage assays**

Primary HUVECs were used to determine the cytotoxicity and efficacy of the NCL-EPO-NP in preventing damage by *C. albicans*. HUVECs were isolated and propagated by the method of Jaffe and colleagues [84]. The cells were grown in M-199 (Gibco, Grand Island, NY) supplemented with 10% fetal bovine serum, 10% defined bovine calf serum, and 2 nM l-glutamine, with penicillin and streptomycin. Second- or third-passage endothelial cells were grown on collagen matrix on 96-well microtiter plates. Treatment with NCL-EPO-NP was conducted in M-199 medium. Different concentrations of the NPs were introduced into the cell lines, and the wells were also added with $1 \times 10^5$ *C. albicans* yeast cells. Plates were incubated for 6 hours at 37˚C in 5% CO$_2$. Damage to HUVEC cells were measured using the chromium release assay well published previously by our group [25,85].

**Animal models**

All animal related study procedures were compliant with the Animal Welfare Act, the Guide for the Care and Use of Laboratory Animals, and the Office of Laboratory Animal Welfare and were conducted under an IACUC approved protocol 31443–03 by The Lundquist Institute at Harbor-UCLA Medical Center.

**Mouse model of oropharyngeal candidiasis (OPC)**

Male, 6-week-old CD1 mice were purchased from Taconic. OPC was induced in mice as described previously [38]. Mice were injected subcutaneously with cortisone acetate (225 mg/kg of body weight) on days −1, 1, and 3 relative to infection. For inoculation, the animals were sedated, and a swab saturated with $2 \times 10^7$ *C. albicans* cells was placed sublingually for 75 minutes. Mice were either treated intraperitoneally (IP) with 10 mg/kg fluconazole on days 3 and 4 after infection. Some mice were treated intraorally with 200 μg of NCL-EPO-NP on days 1 to 4. Mice were killed on day 5 after infection. The tongues were harvested, weighed, homogenized for 30 seconds, and quantitatively cultured. Some tongues were fixed in zinc-buffered formalin, embedded in paraffin, sectioned, and stained with PAS.
Mouse model of vulvovaginal candidiasis

Mice were infected vaginally using a previously well-published protocol [79]. Five- to 6-week-old female CD1 mice were injected with 0.1 mL of β-Estradiol 17-valerate in sesame oil, subcutaneously in the back of the neck on day −3 and +3 relative to infection using a needle size of 20G to 27G. For inoculation, the mice were anaesthetized by IP injection of a mixture of ketamine (82.5 mg/kg) and xylazine (6 mg/kg). Next, 20 μL of PBS containing $5 \times 10^6$ C. albicans blastospores was injected into the vaginal lumen. A group of mice were also treated intravaginally with fluconazole or NCL-EPO-NP (fluconazole: 10 mg/kg IP once on days 3 and 4 after infection; NCL-EPO-NP: 200 μg intravaginally on days 1 to 4). On day 5 postinfection, vaginas and approximately 1 cm of each uterine horn was dissected, homogenized, and quantitatively cultured.

Supporting information

**S1 Supporting information. Results of the HTS and shortlisting of hits.**

(PDF)

**S1 Fig.** UV-Visible spectra of NCL (NCL-10 ppm), NCL-EPO NPs (equivalent to 10 ppm NCL), and EPO blank NPs (A). Calibration curve for NCL using UV-Vis Spectroscopy ($n = 3 \pm \text{SD}$) (B). Summary of the characteristic FT-IR peaks representing the key functional groups in Eudragit EPO, NCL, Kolliphor P407, and NCL-EPO-NPs (freeze dried) (C). 1H NMR chemical shifts observed in freeze-dried NCL-EPO-NPs in comparison with EPO and NCL (D). Evaluation of particle size, PDI, and zeta potential of NCL-EPO-NPs containing different loading of NCL (% w/w EPO) on long-term storage at room temperature. (Data expressed as mean ± SD; $n = 3$) (E). Raw data are found in the file S1 Data. FT-IR, Fourier-transform infrared; NCL, niclosamide; NCL-EPO-NP, NCL-loaded EPO NP; NP, nanoparticle; PDI, polydispersity index.

(TIF)

**S2 Fig.** NCL-EPO-NPs prevent planktonic C. albicans growth in acetate (A), protect HUVEC from damage (B), penetrate C. albicans biofilms (C), and increase ROS activity in the fungus (D). Raw data are found in the file S1 Data. HUVEC, human umbilical vascular endothelial cell; NCL-EPO-NP, NCL-loaded EPO NP; ROS, reactive oxygen species.

(TIF)

**S3 Fig.** NCL-EPO-NPs reduce oxygen consumption rate in C. albicans—a time course analysis (A). NCL-EPO-NPs can be formulated as gel (B). Histology pictures from the OPC model, 40X magnification, scale = 20 μm (C). Fungal burden in vagina after drug treatment (D). Raw data are found in the file S1 Data. NCL-EPO-NP, NCL-loaded EPO NP; OPC, oropharyngeal candidiasis.

(TIF)

**S4 Fig.** NCL-EPO-NP reduces C. albicans growth and filamentation at approximately 0.5 μg/ml in both YP+1% glucose or RPMI medium (when cells remain in the yeast form, they fall to the bottom of the round-bottom wells forming a ring that is easily identifiable by the naked eye; filamentation instead displays a fuzzy circumference [86]). NCL parent is ineffective even at >32 μg/ml (A,B). Parent NCL or NP control did not detach biofilms, while NCL-EPO-NP detached preformed biofilms at concentrations as low as 0.5–1 μg/ml (C). NCL-EPO-NP abrogates filamentation at 1 μg/ml, while parent NCL does not, and filaments as efficiently as the no drug control. NCL, niclosamide; NCL-EPO-NP, NCL-loaded EPO NP;
NP, nanoparticle.

(SI) Data. This file contains numerical values for figures as indicated in the individual sheets.

(Author Contributions)

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