Co-Modification With Mesenchymal Stem Cells Membrane and PDA Prevents Fe3O4-Induced Pulmonary Toxicity in Mice via AMPK-ULK1 Axis

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Research

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Abstract

Background: Fe\textsubscript{3}O\textsubscript{4} nanoparticles are widely used in the diagnosis and treatment of diseases, but the toxicity should not be ignored. It has been reported that PDA modification can reduce the toxicity of Fe\textsubscript{3}O\textsubscript{4} and increase the biocompatibility. However, a better modification method is still worth studying. We have developed a new method to coat Fe\textsubscript{3}O\textsubscript{4}@PDA nanoparticles with mesenchymal stem cells membrane (MSCM) and evaluated the lung toxicity of the modified particles to mice.

Result: We found that MSCM modification significantly reduced the lung injury induced by Fe\textsubscript{3}O\textsubscript{4} nanoparticles in mice. Compared with Fe\textsubscript{3}O\textsubscript{4}@PDA nanoparticles, co-modification with MSCM and PDA modification significantly reduced autophagy and apoptosis of mouse lung tissue, and reduced the activation of autophagy pathway AMPK-ULK1 axis. Thus, co-modification with MSCM and PDA prevents Fe\textsubscript{3}O\textsubscript{4}-induced pulmonary toxicity in mice by inhibiting the AMPK-ULK1 derived autophagy.

Conclusion: MSCM coated Fe\textsubscript{3}O\textsubscript{4}@PDA nanoparticles were demonstrated to prevent lung damage from autophagy and reduce the toxicity of iron oxide nanomaterials. The co-modification of PDA and MSCM can improve the biocompatibility and facilitate their further bioapplication.

Background

Nano-sized Fe\textsubscript{3}O\textsubscript{4} has many special properties, such as superparamagnetism, which enables it to be used as magnetic resonance imaging contrast agents\cite{1}, targeted drug delivery systems\cite{2} and hyperthermic agents\cite{3}. However, the negative effects of nano-sized Fe\textsubscript{3}O\textsubscript{4} in practical application should not be ignored. Some studies have shown that metal oxides, including Fe\textsubscript{2}O\textsubscript{3}, Fe\textsubscript{3}O\textsubscript{4} and ZnO can induce autophagy in vivo\cite{4,5}. In addition, it has been reported that in the process of drug treatment with nanoparticles, nanoparticles not only induce autophagy of specific lesions, but also induce autophagy of normal cells, leading to poisoning of healthy cells\cite{6}.

As the most abundant organ of blood flow, pulmonary macrophages absorb nanoparticles through endocytosis and cause lung damage\cite{7–9}. Nano titanium exposure induces dose- and size-dependent cytotoxicity on human epithelial lung cells\cite{10}. Nano NiO can lead to lung injury in rats which may be related with nitrative stress reaction based on pulmonary inflammation\cite{11}. Little is known about the role of Fe\textsubscript{3}O\textsubscript{4} in pulmonary toxicity, nor the mechanisms of Fe\textsubscript{3}O\textsubscript{4}-induced autophagy.

Before being used in medicine, the nanoparticles must be modified with some molecular layers to produce biocompatibility. Dopamine is one of the main pigments of melanin, which is rich in neurotransmitter in human body. This neurotransmitter can self-aggregate to form polydopamine (PDA) under specific conditions. Because of the high biocompatibility and biodegradability, PDA has been widely used in the camouflage of nanoparticles and various biomedical applications\cite{12}. PDA-coated magnetic nanostructures have good thermal stability, photothermal conversion efficiencies, pH responsiveness, biocompatibility and low genotoxicity\cite{13–15}. Some studies have shown that the use of PDA modification can significantly improve the biocompatibility of Fe\textsubscript{3}O\textsubscript{4}, but it still shows a certain degree of cytotoxicity. Therefore, the development of new modification methods is an urgent need for the clinical application of Fe\textsubscript{3}O\textsubscript{4}. 
The natural stem cell membrane camouflaged nanoparticles were used as new drug delivery carriers[16]. The new drug delivery carrier first separated the mesenchymal stem cell membrane, and then obtained the nanoparticles camouflaged by the physical extrusion method. By passing the “passport” to these nanomaterials, the immune system avoids external rejection of particles, thereby avoiding the occurrence of immune responses[17]. The nanoparticles camouflaged by stem cell membrane have the advantages of uniform particle size, good stability and biocompatibility.

Herein, we have developed a new surface modification method of Fe$_3$O$_4$, that is, the surface of Fe$_3$O$_4$ is modified by mesenchymal stem cell membrane (MSCM) after it is coated with PDA. Compared with Fe$_3$O$_4$@PDA particles, this modified method has better biocompatibility and less lung damage. In addition, we also explored the mechanism of lung injury induced by Fe$_3$O$_4$. MSCM modification apparently avoided most of the autophagy induced by Fe$_3$O$_4$, and the autophagy related AMPK-ULK1 pathway activation was obviously lower.

Materials And Methods

Preparation of Fe$_3$O$_4$ and Fe$_3$O$_4$@PDA

Fe$_3$O$_4$ nanoparticles stabilized by oleic acid were prepared by thermal decomposition method. In short, 2mM of iron acetylacetonate, 5mM of 1,2-hexadecanediol, 6mM of oleic acid and 6mM of oleyl ammonia were mixed in 20mL of dibenzyl ether and mixed under nitrogen for 15min, and then heated to 200 ºC. After 30 min of reaction, it was vortexed at 265 ºC for another 30 min and cooled to room temperature. The oleic acid-stabilized Fe$_3$O$_4$ nanoparticles were separated by a magnet, then washed with n-hexane and ethanol back precipitation three times, and then dispersed in toluene. Then disperse Fe3O4 nanoparticles and super particles in Tris buffer solution (10mM, pH8.5), add PDA hydrochloride monomer and stir for 3h, and then wash the centrifugal washing to remove excess self-polymerized dopamine in the solution to obtain Fe$_3$O$_4$@PDA superparamagnetic nanoparticles.

Preparation of Cells and MSCM-Fe$_3$O$_4$@PDA

MSCs were purchased from American Type Culture Collection (Manassas, VA, USA). They were cultured in DMEM α supplemented with 10% FBS in a humidified atmosphere of 5% CO$_2$ at 37°C. The suspended cells were washed 3 times with PBS and centrifuged. Then, the cell pellet was suspended in a mixture of 225 mM d-mannitol, 20 mM Tris-HCl (pH 7.5), 75 mM sucrose and 0.2 mM EGTA for 24 hours to allow them to completely dissolve. The cells were then disrupted using a Dounce homogenizer at 4 ºC. After centrifuging at 3500 g for 5 min at 4 ºC, the supernatant was kept and centrifuged at 20,000 g for 30 min at 4 ºC. The supernatant was discarded and the membrane of MSCs was collected as an off-white precipitate for subsequent experiments. The MSCM were fully dispersed in PBS, and cell membrane vesicles were prepared using Avanti micro extruder. MSCM vesicles and Fe$_3$O$_4$@PDA core were mixed at a weight ratio of polymer to membrane protein of 2: 1 and coextruded through a PDA membrane with a pore size of 200 nm for 10 times to obtain MSCM-Fe$_3$O$_4$@PDA.

Animal experiment

As shown in Figure.1, 48 ICR mice weighing 18-22 g were purchased from SPF Biotechnology (Beijing, China) and were randomized into four groups: saline, Fe$_3$O$_4$, Fe$_3$O$_4$@PDA and MSCM-Fe$_3$O$_4$@PDA exposure groups. Drug was injected into mice via tail vein. The dosage of Fe$^{3+}$ was 45 mg/kg.kw/d (1/10 LD$_{50}$). After four weeks, the mice were euthanized. According to the previously described method, the lungs were taken out and lavaged using 500
μL PBS for three times to obtain a total of 1500 μL of bronchoalveolar lavage fluid (BALF). Then half of the lungs of each group were stored at -80 degrees to extract protein and mRNA, and the rest were fixed with 4% formalin and stored at room temperature for staining.

**H&E staining**

Paraffin sections were dewaxed to water, dyed with Harris hematoxylin for 3-8 min and washed with water. Then the sections were immersed in 1% Hydrochloric acid alcohol for several seconds and washed with water. Next, the sections were dyed in eosin solution for 1-3 min, then dehydrated gradiently and sealed with gum. The sections were observed under microscope and the images were collected.

**Western blotting**

The mice lung tissues were lysed with ice-cold RIPA lysis buffer containing phosphatase-protease inhibitor cocktails (Beyotime Biotechnology, Shanghai, China). The concentration of protein was measured by BCA Protein Assay Kit (Beyotime Biotechnology, Shanghai, China). Equal amounts of protein lysates were subjected to SDS gel electrophoresis, immunoblotted with primary antibodies, and then the matched secondary antibodies. Western blot results were quantified by using the Image J software. Antibodies: Bax Rabbit Polyclonal antibody (Proteintech, CN, 50599-2-lg); Bcl-2 Rabbit Polyclonal antibody (Proteintech, CN, 12789-1-AP); Cleaved Caspase-3 Rabbit Polyclonal antibody (Cell Signaling Technology, US, 9664); Cleaved Caspase-9 Mouse Polyclonal antibody (Cell Signaling Technology, US, 9509); Beclin1 Rabbit Polyclonal antibody (Proteintech, CN, 11306-1-AP); P62 Rabbit Polyclonal antibody (Proteintech, CN, 18420-1-AP); LC3 Rabbit Polyclonal antibody (Proteintech, CN, 14600-1-AP); LC3-II Rabbit Polyclonal antibody (Cell Signaling Technology, US, 3868); p-AMPK Rabbit Polyclonal antibody (Cell Signaling Technology, US, 4186); AMPK Rabbit Polyclonal antibody (Proteintech, CN, 10929-2-AP); p-ULK1 Rabbit Polyclonal antibody (Cell Signaling Technology, US, 37762); ULK1 Rabbit Polyclonal antibody (Proteintech, CN, 20986-1-AP).

**RNA isolation and qRT-PCR**

Total RNA was extracted from tissues using TRIzol (Invitrogen) following the manufacturer’s instructions. 1mg of total RNA was subjected to reverse transcription using the One-Step cDNA Synene, Beijing, China) was used for RT-qPCR. The PCR primer sequences are shown as Table 1.

**Table 1 Primers Used for qPCR**
| Target gene | Direction | Sequence               |
|-------------|-----------|------------------------|
| Bcl-2       | Forward   | CAGAGGGGCTACGAGTGGGATG |
|             | Reverse   | TGGGTGGCTCTCAGGCTGGAAG |
| Bax         | Forward   | TGCTGACGTGGACACGGACTC  |
|             | Reverse   | AGCAAAAGTAGAAGGGCAACCAC |
| AMPK        | Forward   | ACACGGGAGGGTTGAAGAGG   |
|             | Reverse   | AGAATCTGCTGGAAGAGCCG   |
|ULK1         | Forward   | TCCCTACACACCTTCTCCCC   |
|             | Reverse   | TCTGGTACGGGTACTCTGGG   |
| β-actin     | Forward   | CACCCGCGAGTACAACCTTC   |
|             | Reverse   | CCCATACCACCACATCACACC  |

**Immunocytochemistry**

Tissue slides were deparaffinized and rehydrated, then incubated with primary antibodies overnight at 4 °C. Next, the sections were incubated with matched secondary antibody for 30 minutes at room temperature, stained with DAB, and counterstained with hematoxylin.

**Statistical analysis**

All statistical analyses were carried out using the SPSS 19.0 statistical software package (SPSS Inc., Chicago, IL, USA). The data were presented as the mean ± standard deviation (SD) at least three independent experiments. For the analysis of IHC pictures, 5 visual fields were randomly selected to take photos, and the average score was calculated. Data were analyzed using one-way analysis of variance for comparison between groups. *p<0.05* was statistically significant.

**Results**

**Characterization of Fe₃O₄, Fe₃O₄@PDA and MSCM-Fe₃O₄@PDA**

Through TEM observation, Fe₃O₄, Fe₃O₄@PDA and MSCM-Fe₃O₄@PDA all showed uniform spherical structure, while MSCM-Fe₃O₄@PDA camouflaged with MSCM showed spherical core-shell structure, which indicated that MSCM had successfully camouflaged on the surface of Fe₃O₄@PDA (Figure.2A). Compared with Fe₃O₄@PDA, the average hydrodynamic diameter of MSCM-Fe₃O₄@PDA increased from 70.6±0.8 nm to 85.4±1.4 nm, which was basically consistent with the results of TEM. The increase in diameter may be due to the thickness of MSCM produced by lipid bilayer (Figure.2B).

The protein bands of Na⁺-K⁺-ATPase and CXCR4 were clearly observed on the surface of MSCM-Fe₃O₄@PDA, the lysate of MSCs and the membrane of MSCs (Figure.2C). In addition, GAPDH bands were clearly observed in the cracking solution of MSCs, but almost no in the MSCM-Fe₃O₄@PDA nanoparticles and MSCs membrane, which
indicated the purity of MSCM, and confirmed that the surface of Fe$_3$O$_4$@PDA was successfully camouflaged by MSCM.

**Co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced lung injury in mice**

The total amount of protein and neutrophils in BALF can reflect the lung damage of mice. As shown in Table 2, we found that compared with Fe$_3$O$_4$ group, the amount of total protein and neutrophils in BALF of Fe$_3$O$_4$@PDA group and MSCM-Fe$_3$O$_4$@PDA group decreased significantly. Compared with Fe$_3$O$_4$@PDA group, the amount of total protein and neutrophil number of MSCM-Fe$_3$O$_4$@PDA were more reduced. We then measured the level of inflammatory factors in BALF. The ELISA assay showed that the expression of IL-6 and IL-8 in mice exposed to Fe$_3$O$_4$ increased significantly, while the level of inflammatory factors induced in Fe$_3$O$_4$@PDA group, and further decreased in MSCM-Fe$_3$O$_4$@PDA group. The results showed that the co-modification of MSCM and PDA increased the biocompatibility of Fe$_3$O$_4$ nanoparticles and reduced lung injury in mice.

**Table 2 Detection of inflammatory factors in BALF of mice (mean±sd)**

| Factors              | Total protein concentration | Number of neutrophils | IL-6 (pg/mL) | IL-8 (pg/mL) | TNF-α (pg/mL) |
|----------------------|-----------------------------|-----------------------|--------------|--------------|---------------|
| Saline               | 98.33±8.50                  | 4536.67 ± 152.88      | 1.72 ±0.17   | 1.70±0.29    | 4.08±0.43     |
| Fe$_3$O$_4$          | 497.00±9.54$^a$             | 23153.67 ± 530.10$^a$ | 72.82 ± 7.64 | 55.16±3.81$^a$ | 106.76±6.64$^a$ |
| Fe$_3$O$_4$@PDA      | 437.67±8.33$^{ab}$          | 15758.00±1642.74$^{ab}$ | 52.54 ±5.09$^{ab}$ | 35.52±4.73$^{ab}$ | 83.94±2.80$^{ab}$ |
| MSCM-Fe$_3$O$_4$@PDA | 392.67±20.53$^{abc}$       | 11287.33±781.47$^{abc}$ | 19.18±4.50$^{abc}$ | 19.55±0.79$^{abc}$ | 34.39±10.91$^{abc}$ |
| $F$ value            | 576.68                      | 203.00                | 117.89       | 165.20       | 151.97        |
| $p$ value            | <0.001                      | <0.001                | <0.001       | <0.001       | <0.001        |

($^a$: Significant compared with the Saline group; $^b$: Significant compared with the Fe$_3$O$_4$ group; $^c$: Significant compared with the Fe$_3$O$_4$@PDA group)

**Co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced apoptosis of lung tissue**

HE staining was used to detect the pathological morphology of the lungs of mice (Figure.3A). The results showed that Fe$_3$O$_4$ induced significant pathological changes in the alveoli of mice, including thickening of alveoli, hemorrhage and edema of alveoli, and infiltration of inflammatory cells. No pathological changes were observed in the lungs of mice exposed to MSCM-Fe$_3$O$_4$@PDA. We then used TUNEL staining to detect the apoptosis of lung cells in mice. The results showed that Fe$_3$O$_4$ significantly induced the apoptosis of mouse lung cells, PDA modification reduced the apoptosis rate, and MSCM modification further reduced the apoptosis of mouse lung cells (Figure.3B, Figure.3C). Western blotting (Figure.3D) and PCR (Figure.3E) showed that MSCM modification significantly inhibited the increase of Bax induced by Fe$_3$O$_4$. For Bcl-2, MSCM-Fe$_3$O$_4$@PDA significantly increased its expression, compared with Fe$_3$O$_4$@PDA group.
We next performed IHC staining to detect the expression of apoptosis related proteins in mouse lung tissue (Figure.4A). The results showed that Fe$_3$O$_4$ significantly increased the expression of Bax (Figure.4B), Caspase-3 (Figure.4D) and Caspase-9 (Figure.4E), and decreased the expression of Bcl-2 (Figure.4C), which was consistent with our Western blot results. Compared with the Fe$_3$O$_4$@PDA group, MSCM-Fe$_3$O$_4$@PDA group further reduced the increase of Bax and the decrease of Bcl-2. Those results show that co-modification with MSC and PDA prevents Fe$_3$O$_4$-induced apoptosis of lung tissue.

**Co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced autophagy of lung tissue**

It has been reported that nanoparticles lead to apoptosis by inducing autophagy. We then detected autophagy makers in the lung tissue of mice. It was found that Fe$_3$O$_4$ significantly increased the number of autophagic vesicles in mouse lung cells, while PDA decreased the number of autophagic vesicles, and MSCM further reduced the increase of autophagic vesicles (Figure.5A). Beclin1 is the key regulatory protein of autophagy. As shown in Figure.5B, we found that the expression of Beclin1 protein in the lungs of mice exposed to Fe$_3$O$_4$ increased significantly. Compared with the Fe$_3$O$_4$@PDA group, the expression of Beclin1 protein in the lungs of mice in the MSCM-Fe$_3$O$_4$@PDA group decreased more obviously. P62 is an intracellular protein induced by stress and acts on selective autophagy. We found that the expression of p62 protein in lung of mice exposed to Fe$_3$O$_4$ decreased significantly, while the original level of p62 protein could be restored by MSCM modification. LC3 is a marker of autophagy. When autophagy is formed, cytoplasmic LC3 (LC3-I) will hydrolyze a small peptide and change into membrane type (LC3-II). The ratio of LC3-II/I can estimate the level of autophagy. We detected the LC3-II/I ratio of lung in four groups of mice by Western blotting. The results showed that MSCM-Fe$_3$O$_4$@PDA significantly inhibited the increase of LC3-II/I ratio induced by Fe$_3$O$_4$. IHC staining (Figure.6A) of Beclin1 (Figure.6B), p62 (Figure.6C) and LC3-II (Figure.6D) protein in mouse lung was consistent with Western blot. These results indicate that co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced autophagy of lung tissue.

**Co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced activation of AMPK-ULK1 axis**

Ulk1 complex can be used as a bridge between upstream energy sensing protein AMPK and downstream autophagy formation. Ulk1 is highly phosphorylated by AMPK, and then Beclin1 is activated, which is necessary for autophagy initiation. We then examined whether co-modification with MSCM and PDA attenuated Fe$_3$O$_4$ induced autophagy by interfering with the AMPK-ULK1 axis, a key regulatory pathway of autophagy. The results of Western blotting (Figure.7A) showed that there was no significant difference in the total protein levels of AMPK and ULK1 in the lung tissues among groups. However, Fe$_3$O$_4$ exposure significantly increased the phosphorylation level of AMPK and ULK1 protein in mice lungs, while PDA and MSCM modification significantly restored the phosphorylation level of AMPK and ULK1 protein. Compared with the Fe$_3$O$_4$@PDA group, the level of p-ULK1 protein in the lung of the MSCM-Fe$_3$O$_4$@PDA group was further reduced. The PCR results (Figure.7B) showed that the expression of AMPK and ULK1 mRNA was no significant affected among groups. The above results show that co-modification with MSCM and PDA prevents Fe$_3$O$_4$-induced activation of AMPK-ULK1 axis.

**Discussion**

Iron oxide nanoparticles have gained extensive attention in biomedicine because of their excellent magnetic properties[18, 19]. Tagged molecule can now be directed to a desired location with help of an external magnet[20]. Only precaution one has to take is to select a magnetic material having low toxicity and its ability for binding a
biomolecules[21]. Unfortunately, unmodified metal nanoparticles are often reported to have toxic effects, including hepatotoxicity[22, 23], nephrotoxicity[24, 25] and myocardial toxicity[26, 27]. In this study, we focused on the lung toxicity induced by Fe$_3$O$_4$ and how to use new modification methods to reduce the negative effects of Fe$_3$O$_4$.

The damage of nanoparticles to organs is usually caused by cell apoptosis. Apoptosis is mainly caused by the activation of caspase, a cysteine protease, by signal stimulation in vitro or intracellular[28]. Autophagy, like apoptosis, is an important physiological response of cells[29]. Under normal physiological conditions, autophagy remains at a low basic level, but it can be induced by some specific cell stress states[30]. Autophagy may have different effects on cells. Under specific circumstances, autophagy can maintain cell survival, which is called protective autophagy[31], and sometimes autophagy can cause secondary apoptosis[32]. We injected Fe$_3$O$_4$ into the tail vein of mice and took out the lungs of mice four weeks later for observation. We found that Fe$_3$O$_4$ led to the destruction of mice lungs and the increase of apoptosis of lung cells. This is consistent with Stern's report[33] that demonstrated elevated levels of autophagic vacuoles upon exposure of cells to certain nanomaterials and the interaction between nanomaterials and the autophagy pathway is disruptive, resulting in obvious morphological changes and finally cell death.

In order to further push the limits of nanoparticle performance and function, a paradigm shift to a bionic design strategy has recently emerged[34]. A new class of biomimetic nanoparticle has been reported that combines the advantages of natural, cell membrane-derived vesicles with more traditional synthetic nanoparticulate platforms[35, 36]. This new coating technology of grafting the cell membrane onto the surface of nanoparticles has pushed the nanomedicine to a new stage of development. The camouflaged nanoparticles can better adapt to the complex physiological environment[37]. Through homologous recognition, they can not only avoid the elimination of the immune system, but also greatly enhance the targeting characteristics, which has great application potential.

These particles generally employ a core-shell design, with a layer of cell membrane coated around a preformed nanoparticle core. Initially, membrane-coated nanoparticles were fabricated using a combination of red blood cell membrane and poly(lactic-co-glycolic acid), a biodegradable polymer, via a co-extrusion approach[38]. In this experiment, we used the umbilical cord derived MSCM as a vesicle to wrap PDA modified Fe$_3$O$_4$ particles. Given the demonstrated low immunogenicity and strong targeting of stem cell membrane[39], we hypothesized that this new modification technology can greatly reduce the organ toxicity of Fe$_3$O$_4$ particles in vivo.

It is worth noting that mice injected with Fe$_3$O$_4$ particles coated with MSCM showed significantly lower lung injury, lower apoptosis and autophagy levels, which indicated that the co-modification of MSCM and PDA could significantly improve the biocompatibility of Fe$_3$O$_4$ particles modified by PDA alone.

Recently, it has been established that there is a direct link between AMPK, which is an energy sensor and is activated by glucose starvation[40], and ULK1 in triggering autophagy. Based on their doses and physico-chemical characteristics, nanoparticles have the capability of producing reactive oxygen species (ROS) or otherwise initiating signaling pathways that in addition to regulating autophagy, can eventually modulate different cell fates, including necrosis, necroptosis, apoptosis[41]. The intrinsic pathway of apoptosis is initiated by mitochondrial membrane permeabilization, various types of oxidative stress including hypoxia, DNA damage, and growth-factor deprivation[42]. Mitochondrial ROS production is a tightly regulated redox signal that transmits information from the organelle to the cell[43]. It has been proposed that ROS can directly regulate AMPK activity independently of changes in adenine nucleotides[44, 45]. Our results show that MSCM can significantly reduce the activation of
AMPK-ULK1 induced by Fe₃O₄ particles, which suggests that the protective effect of MSCM on mice lung may be achieved by reducing the level of oxidative stress, which should be discussed in the further experiments. Although PDA modification has attenuated the lung toxicity of Fe₃O₄ particles, we found that Fe₃O₄ particles encapsulated in stem cell membrane induce lower lung injury, autophagy and apoptosis than Fe₃O₄ particles modified by PDA alone. Thus, MSCM-coated Fe₃O₄@PDA might be safely used for drug delivery and disease diagnosis.

**Conclusion**

In this study, we developed a new surface modification method of Fe₃O₄ particles, that is, MSCM was used to wrap Fe₃O₄@PDA particles, and proved its good biocompatibility through animal experiments. Co-modification with MSCM and PDA prevents Fe₃O₄-induced Pulmonary toxicity in mice by inhibiting the AMPK-ULK1 derived autophagy, which makes MSCM-coated Fe₃O₄@PDA particles have strong clinical application potential.

**Abbreviations**

MSCM, Mesenchymal stem cell membrane; PDA, polydopamine; PBS, phosphate buffer solution; BALF, bronchoalveolar lavage fluid; ELISA, enzyme linked immunosorbent assay; H&E, hematoxylin-eosin; IHC, immunohistochemistry; TEM, transmission electron microscopy; SD, standard deviation; ROS, reactive oxygen species; AMPK, AMP-activated protein kinase; ULK1, unc-51 like autophagy activating kinase 1.

**Declarations**

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**Authors' contributions**

Te Liu, Jinlan Jiang conceived and designed the experiments; Te Liu, Hua Yao, Jun Yan, Pu Shao, Yuzhuo Wang, Tianxin Liu performed the experiments; Te Liu collected the data; Hua Yao, Jun Yan, Tianxin Liu analyzed the data; Te Liu wrote the paper. All authors checked and approved the final manuscript.

**Conflicts of interest**

The authors report no conflicts of interest in this work.

**Ethics approval and consent to participate**

All the experiments involved animals were meet the requirements. The animal experimental ethical inspection of this research was done by institutional animal care and use committee of Jilin University. The number of permit is KT201901003.

**Consent for publication**
Informed consent for publication was obtained from all participants. All the authors have agreed to publish this research.

**Availability of data and materials**

All data generated or analysed during this study are included in this published article. The datasets used or analysed during the current study are available from the corresponding author on reasonable request.

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**References**

1. Wang G, Zhang X, Skallberg A, Liu Y, Hu Z, Mei X, Uvdal K: One-step synthesis of water-dispersible ultra-small Fe3O4 nanoparticles as contrast agents for T1 and T2 magnetic resonance imaging. *Nanoscale* 2014, 6:2953-2963.

2. Vangijzegem T, Stanicki D, Laurent S: Magnetic iron oxide nanoparticles for drug delivery: applications and characteristics. *Expert Opin Drug Deliv* 2019, 16:69-78.

3. Dunn AW, Ehsan SM, Mast D, Pauletti GM, Xu H, Zhang J, Ewing RC, Shi D: Photothermal effects and toxicity of Fe3O4 nanoparticles via near infrared laser irradiation for cancer therapy. *Mater Sci Eng C Mater Biol Appl* 2015, 46:97-102.

4. Khan MI, Mohammad A, Patil G, Naqvi SA, Chauhan LK, Ahmad I: Induction of ROS, mitochondrial damage and autophagy in lung epithelial cancer cells by iron oxide nanoparticles. *Biomaterials* 2012, 33:1477-1488.

5. Liu Y, Li X, Bao S, Lu Z, Li Q, Li CM: Plastic protein microarray to investigate the molecular pathways of magnetic nanoparticle-induced nanotoxicity. *Nanotechnology* 2013, 24:175501.

6. Lewinski N, Colvin V, Drezek R: Cytotoxicity of nanoparticles. *Small* 2008, 4:26-49.

7. Kobayashi N, Naya M, Endoh S, Maru J, Yamamoto K, Nakanishi J: Comparative pulmonary toxicity study of nano-TiO(2) particles of different sizes and agglomerations in rats: different short- and long-term post-instillation results. *Toxicology* 2009, 264:110-118.

8. Nishimori H, Kondoh M, Isoda K, Tsunoda S, Tsutsumi Y, Yagi K: Histological analysis of 70-nm silica particles-induced chronic toxicity in mice. *Eur J Pharm Biopharm* 2009, 72:626-629.

9. Su Y, Xu JY, Shen P, Li J, Wang L, Li Q, Li W, Xu GT, Fan C, Huang Q: Cellular uptake and cytotoxic evaluation of fullerol in different cell lines. *Toxicology* 2010, 269:155-159.

10. Gandamalla D, Lingabathula H, Yellu N: Nano titanium exposure induces dose- and size-dependent cytotoxicity on human epithelial lung and colon cells. *Drug Chem Toxicol* 2019, 42:24-34.

11. Liu S, Zhu A, Chang X, Sun Y, Zhou H, Zou L, Su L: Role of nitrate stress in nano nickel oxide-induced lung injury in rats. *Wei Sheng Yan Jiu* 2016, 45:563-567.
12. Lynge ME, Schattling P, Stadler B: Recent developments in poly(dopamine)-based coatings for biomedical applications. *Nanomedicine (Lond)* 2015, **10**:2725-2742.

13. Fan X, Yuan Z, Shou C, Fan G, Wang H, Gao F, Rui Y, Xu K, Yin P: cRGD-Conjugated Fe3O4@PDA-DOX Multifunctional Nanocomposites for MRI and Antitumor Chemo-Photothermal Therapy. *Int J Nanomedicine* 2019, **14**:9631-9645.

14. Wozniak A, Walawender M, Tempka D, Coy E, Zaleski K, Grzeskowiak BF, Mrowczynski R: In vitro genotoxicity and cytotoxicity of polydopamine-coated magnetic nanostructures. *Toxicol In Vitro* 2017, **44**:256-265.

15. Song X, Gu X, Sun H, Fu C, Zhang Y, Dong P: Biomimetic Modification and In Vivo Safety Assessment of Superparamagnetic Iron Oxide Nanoparticles. *J Nanosci Nanotechnol* 2016, **16**:4100-4107.

16. Bose RJ, Kim BJ, Arai Y, Han IB, Moon JJ, Paulmurugan R, Park H, Lee SH: Bioengineered stem cell membrane functionalized nanocarriers for therapeutic targeting of severe hindlimb ischemia. *Biomaterials* 2018, **185**:360-370.

17. Narain A, Asawa S, Chhabria V, Patil-Sen Y: Cell membrane coated nanoparticles: next-generation therapeutics. *Nanomedicine (Lond)* 2017, **12**:2677-2692.

18. Martinkova P, Brtnicky M, Kynicky J, Pohanka M: Iron Oxide Nanoparticles: Innovative Tool in Cancer Diagnosis and Therapy. *Adv Healthc Mater* 2018, **7**.

19. Laurent S, Forge D, Port M, Roch A, Robic C, Vander Elst L, Muller RN: Magnetic iron oxide nanoparticles: synthesis, stabilization, vectorization, physicochemical characterizations, and biological applications. *Chem Rev* 2008, **108**:2064-2110.

20. Jurek PM, Zablocki K, Wasko U, Mazurek MP, Otlewski J, Jelen F: Anti-FGFR1 aptamer-tagged superparamagnetic conjugates for anticancer hyperthermia therapy. *Int J Nanomedicine* 2017, **12**:2941-2950.

21. Mehta RV: Synthesis of magnetic nanoparticles and their dispersions with special reference to applications in biomedicine and biotechnology. *Mater Sci Eng C Mater Biol Appl* 2017, **79**:901-916.

22. Sha B, Gao W, Wang S, Gou X, Li W, Liang X, Xu Z, Xu F, Lu TJ: Oxidative stress induced hepatotoxicity induced by nano-titanium dioxide in BRL-3A cells and Sprague-Dawley rats. *J Appl Toxicol* 2014, **34**:345-356.

23. Yang B, Wang Q, Lei R, Wu C, Shi C, Yuan Y, Wang Y, Luo Y, Hu Z, Ma H, Liao M: Systems toxicology used in nanotoxicology: mechanistic insights into the hepatotoxicity of nano-copper particles from toxicogenomics. *J Nanosci Nanotechnol* 2010, **10**:8527-8537.

24. Lei R, Wu C, Yang B, Ma H, Shi C, Wang Q, Yuan Y, Liao M: Integrated metabolomic analysis of the nano-sized copper particle-induced hepatotoxicity and nephrotoxicity in rats: a rapid in vivo screening method for nanotoxicity. *Toxicol Appl Pharmacol* 2008, **232**:292-301.

25. Uzar NK, Abudayyak M, Akcay N, Algun G, Ozhan G: Zinc oxide nanoparticles induced cyto- and genotoxicity in kidney epithelial cells. *Toxicol Mech Methods* 2015, **25**:334-339.

26. Fang Y, Wang H, Dou HJ, Fan X, Fei XC, Wang L, Cheng S, Janin A, Zhao WL: Doxorubicin-loaded dextran-based nano-carriers for highly efficient inhibition of lymphoma cell growth and synchronous reduction of cardiac toxicity. *Int J Nanomedicine* 2018, **13**:5673-5683.

27. Khosravi Y, Salimi A, Pourahmad J, Naserzadeh P, Seydi E: Inhalation exposure of nano diamond induced oxidative stress in lung, heart and brain. *Xenobiotica* 2018, **48**:860-866.

28. Elmore S: Apoptosis: a review of programmed cell death. *Toxicol Pathol* 2007, **35**:495-516.

29. Ravanan P, Srikumar IF, Talwar P: Autophagy: The spotlight for cellular stress responses. *Life Sci* 2017, **188**:53-67.
30. Kroemer G, Marino G, Levine B: Autophagy and the integrated stress response. Mol Cell 2010, 40:280-293.
31. Mathew R, Karantza-Wadsworth V, White E: Role of autophagy in cancer. Nat Rev Cancer 2007, 7:961-967.
32. Kasprzewska-Liskiewicz D: The cell on the edge of life and death: Crosstalk between autophagy and apoptosis. Postepy Hig Med Dosw (Online) 2017, 71:825-841.
33. Stem ST, Johnson DN: Role for nanomaterial-autophagy interaction in neurodegenerative disease. Autophagy 2008, 4:1097-1100.
34. Vijayan V, Uthaman S, Park IK: Cell Membrane Coated Nanoparticles: An Emerging Biomimetic Nanoplatform for Targeted Bioimaging and Therapy. Adv Exp Med Biol 2018, 1064:45-59.
35. Xia Q, Zhang Y, Li Z, Hou X, Feng N: Red blood cell membrane-camouflaged nanoparticles: a novel drug delivery system for antitumor application. Acta Pharm Sin B 2019, 9:675-689.
36. Jiang Q, Liu Y, Guo R, Yao X, Sung S, Pang Z, Yang W: Erythrocyte-cancer hybrid membrane-camouflaged melanin nanoparticles for enhancing photothermal therapy efficacy in tumors. Biomaterials 2019, 192:292-308.
37. Zou H, Zhu J, Huang DS: Cell membrane capsule: a novel natural tool for antitumour drug delivery. Expert Opin Drug Deliv 2019, 16:251-269.
38. Hu CM, Zhang L, Aryal S, Cheung C, Fang RH: Erythrocyte membrane-camouflaged polymeric nanoparticles as a biomimetic delivery platform. Proc Natl Acad Sci U S A 2011, 108:10980-10985.
39. Yang N, Ding Y, Zhang Y, Wang B, Zhao X, Cheng K, Huang Y, Taleb M, Zhao J, Dong WF, et al: Surface Functionalization of Polymeric Nanoparticles with Umbilical Cord-Derived Mesenchymal Stem Cell Membrane for Tumor-Targeted Therapy. ACS Appl Mater Interfaces 2018, 10:22963-22973.
40. Tamargo-Gomez I, Marino G: AMPK: Regulation of Metabolic Dynamics in the Context of Autophagy. Int J Mol Sci 2018, 19.
41. Abdal Dayem A, Hossain MK, Lee SB, Kim K, Saha SK, Yang GM, Choi HY, Cho SG: The Role of Reactive Oxygen Species (ROS) in the Biological Activities of Metallic Nanoparticles. Int J Mol Sci 2017, 18.
42. Cavalcante GC, Schaan AP, Cabral GF, Santana-da-Silva MN, Pinto P, Vidal AF, Ribeiro-Dos-Santos A: A Cell’s Fate: An Overview of the Molecular Biology and Genetics of Apoptosis. Int J Mol Sci 2019, 20.
43. Scherz-Shouval R, Elazar Z: Regulation of autophagy by ROS: physiology and pathology. Trends Biochem Sci 2011, 36:30-38.
44. Shao D, Oka S, Liu T, Zhai P, Ago T, Sciarretta S, Li H, Sadoshima J: A redox-dependent mechanism for regulation of AMPK activation by Thioredoxin1 during energy starvation. Cell Metab 2014, 19:232-245.
45. Auciello FR, Ross FA, Ikematsu N, Hardie DG: Oxidative stress activates AMPK in cultured cells primarily by increasing cellular AMP and/or ADP. FEBS Lett 2014, 588:3361-3366.

Figures
As shown in Figure 1, 48 ICR mice weighing 18-22 g were purchased from SPF Biotechnology (Beijing, China) and were randomized into four groups: saline, Fe3O4, Fe3O4@PDA and MSCM-Fe3O4@PDA exposure groups. Drug was injected into mice via tail vein. The dosage of Fe3+ was 45 mg/kg.kw/d (1/10 LD50). After four weeks, the mice were euthanized. According to the previously described method, the lungs were taken out and lavaged using 500 μL PBS for three times to obtain a total of 1500 μL of bronchoalveolar lavage fluid (BALF). Then half of the lungs of each group were stored at -80 degrees to extract protein and mRNA, and the rest were fixed with 4% formalin and stored at room temperature for staining.
Through TEM observation, Fe3O4, Fe3O4@PDA and MSCM-Fe3O4@PDA all showed uniform spherical structure, while MSCM-Fe3O4@PDA camouflaged with MSCM showed spherical core-shell structure, which indicated that MSCM had successfully camouflaged on the surface of Fe3O4@PDA (Figure.2A). Compared with Fe3O4@PDA, the average hydrodynamic diameter of MSCM-Fe3O4@PDA increased from 70.6±0.8nm to 85.4±1.4nm, which was basically consistent with the results of TEM. The increase in diameter may be due to the thickness of MSCM produced by lipid bilayer (Figure.2B). The protein bands of Na+K+-ATPase and CXCR4 were clearly observed on the surface of MSCM-Fe3O4@PDA, the lysate of MSCs and the membrane of MSCs (Figure.2C). In addition, GAPDH bands were clearly observed in the cracking solution of MSCs, but almost no in the MSCM-Fe3O4@PDA nanoparticles and MSCs membrane, which indicated the purity of MSCM, and confirmed that the surface of Fe3O4@PDA was successfully camouflaged by MSCM.
HE staining was used to detect the pathological morphology of the lungs of mice (Figure.3A). The results showed that Fe3O4 induced significant pathological changes in the alveoli of mice, including thickening of alveoli, hemorrhage and edema of alveoli, and infiltration of inflammatory cells. No pathological changes were observed in the lungs of mice exposed to MSCM-Fe3O4@PDA. We then used TUNEL staining to detect the apoptosis of lung cells in mice. The results showed that Fe3O4 significantly induced the apoptosis of mouse lung cells, PDA modification reduced the apoptosis rate, and MSCM modification further reduced the apoptosis of mouse lung cells (Figure.3B, Figure.3C). Western blotting (Figure.3D) and PCR (Figure.3E) showed that MSCM modification significantly inhibited the increase of Bax induced by Fe3O4. For Bcl-2, MSCM-Fe3O4@PDA significantly increased its expression, compared with Fe3O4@PDA group.
Figure 4

We next performed IHC staining to detect the expression of apoptosis related proteins in mouse lung tissue (Figure 4A). The results showed that Fe3O4 significantly increased the expression of Bax (Figure 4B), Caspase-3 (Figure 4D) and Caspase-9 (Figure 4E), and decreased the expression of Bcl-2 (Figure 4C), which was consistent with our Western blot results. Compared with the Fe3O4@PDA group, MSCM-Fe3O4@PDA group further reduced the increase of Bax and the decrease of Bcl-2. Those results show that co-modification with MSC and PDA prevents Fe3O4-induced apoptosis of lung tissue.

Figure 6

The results showed that MSCM-Fe3O4@PDA significantly inhibited the increase of LC3-II/I ratio induced by Fe3O4. IHC staining (Figure 6A) of Beclin1 (Figure 6B), p62 (Figure 6C) and LC3-II (Figure 6D) protein in mouse lung was consistent with Western blot. These results indicate that co-modification with MSCM and PDA prevents Fe3O4-induced autophagy of lung tissue.