Modeling and remodeling effects of intermittent administration of teriparatide (parathyroid hormone 1-34) on bone morphogenetic protein-induced bone in a rat spinal fusion model

Takashi Kaito a,⁎, Tokimitsu Morimoto a, Sadaaki Kanayama a, Satoru Otsuru b, Masafumi Kashi a, Takahiro Makino a, Kazuma Kitaguchi a, Masayuki Furuya a, Ryota Chijimatsu a, Kosuke Ebina a, Hideki Yoshikawa a

a Department of Orthopedic Surgery, Osaka University Graduate School of Medicine, 2-2 Yamadaoka, Suita, Osaka 565-0871, Japan
b Center for Childhood Cancer and Blood Disease, The Research Institute at Nationwide Children's Hospital, 700 Children's Drive, Columbus, OH 43205, USA

1. Introduction

Bone grafting is commonly used to treat skeletal disorders involving bone defects or spinal instability (Steinmann and Herkowitz, 1992). Failure of bony fusion results in pseudarthrosis, pain, and disability (Arrington et al., 1996; Robertson and Wray, 2001; Steinmann and Herkowitz, 1992). Bone morphogenetic protein (BMP) may provide an alternative to bone grafting and is the leading osteoinductive growth factor used clinically in bone-related regenerative medicine today (Boden et al., 2000, 2002; Urist, 1965; Wozney et al., 1988).

Although this therapy is effective, use of high BMP doses can cause complications including inflammatory responses and unintended bone formation; these restrict its widespread application (Shields et al., 2006; Smucker et al., 2006). Improved BMP delivery systems have the potential to produce efficient and spatially controlled bone formation (Kaito et al., 2005). However, modeling and remodeling of BMP-induced bone, processes that occur during normal late-phase fracture healing, have not been investigated thoroughly.

Teriparatide (parathyroid hormone [PTH] 1-34) is the only anabolic agent that has been approved by the U.S. Food and Drug Administration for the treatment of osteoporosis. This hormone has a unique mechanism of action; continuous administration of PTH 1-34 shows a catabolic effect, while intermittent administration demonstrates an anabolic effect (Canalis, 2010; Canalis et al., 2007; Dempster et al., 1993; Jilka, 2007; Tam et al., 1982). Recent studies demonstrated that intermittent
PTH 1-34 administration promoted fracture healing (Aspenberg et al., 2010; Gallacher and Dixon, 2010; Komatsubara et al., 2005; Manabe et al., 2007; Neer et al., 2001). Another study found that intermittent PTH 1-34 administration significantly increased fusion rates and newly formed bone quality, concluding that combined administration of rhBMP-2 and PTH 1-34 had a synergistic effect in a rat model of rhBMP-2-induced spinal fusion. Interestingly, at postoperative week 6, the newly formed bone tissue volume (TV) in rats treated with rhBMP-2 tended to be lower than in animals treated with PTH 1-34 (Morimoto et al., 2014). These findings suggest the possibility that PTH 1-34 influences modeling and remodeling of newly formed bone. However, it is unclear whether the newly formed bone TV was low from the outset or decreased over time in these rats. The purpose of this study was to elucidate the time course of change in TV induced by the administration of PTH1-34 by determining the dimension of the newly formed bone (TV) using serial in vivo micro-computed tomography (CT) and to quantify bone formation and resorption at periosteum and endosteum of the newly formed bone by bone histomorphometry.

2. Materials & methods

2.1. Animal treatments

A total of 37 male, 8-week-old, Sprague-Dawley rats with an initial average body weight of 305.9 g (range, 280–330 g) were obtained from Charles River Laboratories Japan, Inc. (Yokohama, Japan) and used in the present study. All animal procedures were conducted in accordance with the guidelines of the Regulations on Animal Experimentation at Osaka University. The study groups are shown in Table 1.

2.1.1. Administration of PTH 1-34

Rats were treated with subcutaneous injections of either PTH 1-34 (60 µg/kg) 3 times a week (180 µg/kg/week) or 0.9% saline vehicle. Injections commenced 2 weeks prior to surgery, in order to enhance the anabolic effect of PTH 1-34 at the time of surgery, and continued until the animals were euthanized. Animals were weighed every 7–10 days, and injection volumes were adjusted accordingly.

2.1.2. Surgery

Rats were anesthetized with a combination of 0.15 mg/kg of medetomidine (Domitol; Nippon Zenyaku Kogyo Co., Ltd., Fukushima, Japan), 2 mg/kg of midazolam (Dormicum; Astellas Pharma Inc., Tokyo, Japan), and 2.5 mg/kg of butorphanol (Vetorphale; Meiji Seika, Ltd., Tokyo, Japan). In addition, preoperative antibiotic (20,000 U/kg penicillin G; Meiji Seika) was administered subcutaneously. We then surgically induced posterolateral lumbar fusion (Kaito et al., 2013; Morimoto et al., 2014; Wang et al., 2003). A posterior midline skin incision was made, followed by 2 separate paramedian incisions in the lumbar fascia 3 mm from the midline, through which the transverse processes were exposed. The L4 and L5 transverse processes were decorticated using a high-speed burr.

A commercially available absorbable collagen sponge (CollaCote; Zimmer Dental Inc., CA, USA) was cut into 5 × 10 mm fragments and placed in a sterile tube. Phosphate-buffered saline (PBS) or rhBMP-2 (50 µg in PBS) was applied to the sponge just before implantation on each side of the spine. We chose 50 µg rhBMP-2 because this corresponded to a high clinical dose (1500 µg/mL) (Morimoto et al., 2014). The fascia and skin incisions were closed using a 4-0 absorbable suture. The rats were housed in separate cages and allowed to eat and drink ad libitum while their condition was monitored daily.

2.1.3. Calcein double labeling for bone histomorphometry

All rats were injected subcutaneously with 10 mg/kg calcein (Dojindo Laboratories, Kumamoto, Japan) at 5 and 2 days before they were euthanized.

2.1.4. Euthanasia and tissue collection

Immediately prior to euthanizing the rats by anesthetic overdose 12 weeks after surgery, blood samples were collected for analysis of bone metabolism markers and stored at −80 °C. Spinal segments and femurs were harvested and fixed with 10% formalin or 70% ethanol for further assessments.

2.2. Serial bone TV measurement by in vivo micro-CT

The TV of the L4-L5 fusion segments (from the bottom of the L5 transverse process cranially to the top of L4 end plate) was measured in vivo at a resolution of 59 µm at time 0 (just before surgery) and at 2, 6, 8, and 12 weeks after surgery.

2.3. Assessment of L4-L5 fusion

L4-L5 fusion was assessed using the two methods described below. Each was performed in a blinded manner by three independent observers and unanimous agreement was required before these were considered to be fused.

2.3.1. Micro-CT

The spines were scanned using high-resolution micro-CT (R_mCT; Rigaku Mechatronics, Tokyo, Japan) at 90 kV and 200 µA. Visualization and data reconstruction were performed using the TRI/3D-BON (RATOC System Engineering, Tokyo, Japan). Coronal and sagittal L4-L5 images at a resolution of 40 µm/voxel were evaluated for clear evidence of bridging bone formation with cortical continuity between the L4 and L5 transverse processes.

2.3.2. Manual assessment

The explanted lumbar spines were manually tested for intersegmental motion. Any motion detected in the anterior-posterior and left-right direction was considered to indicate a failure of fusion, while the absence of motion was considered to indicate successful fusion.

2.4. Microstructural analysis

The quality of the newly formed fusion mass between the transverse processes was analyzed as described previously (Morimoto et al., 2014). Fusion mass scanning was initiated from the lower endplate level of the L4 vertebral body and continued cranially at 2.0-mm increments (fifty slices) at a resolution of 40 µm/voxel on each side. The bone volume (BV)/TV, trabecular thickness (Tb·Th), trabecular number (Tb·N), trabecular separation (Tb·Sp), thickness of cortical bone (Ct), and cortical bone ratio (Cv/Av) were determined.

2.5. Analysis of the systemic effects of PTH 1-34

The BV/TV ratios of the distal femoral epiphysis and L6 vertebral body were analyzed at 40 µm/voxel. Scanning of the distal femur was initiated at 1.5 mm proximal to the growth plate and continued at 3.0-mm increments (75 slices) in order to exclude the primary spongiosa of the femur. Scanning of the L6 vertebral body was initiated at 1.0 mm cranial to the lower growth plate and continued at 3.2-mm increments (80 slices) in order to exclude the primary spongiosa of the vertebral.

| Table 1 | Treatment groups. |
|---------|-------------------|
|         | Implanted material | Injected material |
| Group A (n = 9) | Collagen carrier | Saline |
| Group B (n = 9) | Collagen carrier | PTH1-34 |
| Group C (n = 10) | Collagen carrier + 50 µg rhBMP-2 | Saline |
| Group D (n = 9) | PTH1-34 | Saline |
2.6. Analysis of serum markers of bone metabolism

Serum bone metabolism markers were analyzed using enzyme-linked immunosorbent assays specific for N-terminal propeptide of type 1 procollagen (P1NP; Rat/Mouse P1NP EIA), type 1 collagen cross-linked C-telopeptides (CTX-1; RatLaps ELISA), and tartrate-resistant acid phosphatase-5b (TRACP-5b; RatTRAP Assay) (all from Immunodiagnostic Systems Limited, Fountain Hills, AZ, USA), and osteocalcin (Rat Osteocalcin EIA Kit; Takara Bio Inc., Shiga, Japan), according to the manufacturers’ instructions. Serum from all animals was measured once for each marker.

2.7. Histologic analysis

Five samples each from group C and group D were prepared for undecalciﬁed bone histomorphometry analysis; the remaining samples were prepared for decalciﬁed histological analysis. The dissected and formalin-ﬁxed spines were demineralized with 50% formic acid and 10% sodium citrate, dehydrated through an ethanol series, and embedd ed in parafﬁn wax. Serial 5-μm coronal sections of the operated segments were cut and stained with hematoxylin and eosin.

2.7.1. Bone histomorphometry

Histomorphometric parameters were analyzed using undecalciﬁed sections of fusion mass in cortical and cancellous bone. Only samples from groups C and D were used for the analysis because of the lack of new bone formation in groups A and B. The dissected lumbar spines were ﬁxed with 70% ethanol, stained with Villanueva bone stain, dehydrated through an ethanol series, and embedded in methyl methacrylate. Static and dynamic bone histomorphometrical measurements of the newly formed bone were performed using a semiautomatic image-analyzing system (System Supply, Nagano, Japan) and a ﬂuorescent microscope at ×320 magniﬁcations. The bone histomorphometric parameters measured were: osteoid and eroded surface/unit bone surface (OS/BS and ES/BS), double-labeled and single-labeled surface/unit BS (dLS/BS and sLS/BS), number of osteoblasts and osteoclasts/unit BS (N·Ob/BS and N·Oc/BS), mineralizing surfaces/unit BS (MS/BS), mineral apposition rate (MAR), and bone formation rate/unit BS (BFR/BS) and bone resorption rate (BRSR) 25.

2.8. Statistical analyses

PASW software (version 18; SPSS, Chicago, IL) was used for all of the analyses. The Mann-Whitney U test was used to compare variables and the level of signiﬁcance was p < 0.05.

3. Results

One rat in group C died just after surgery and another rat in this group died 2 weeks after surgery, following anesthesia for micro-CT; thus, 35 rats were included in the ﬁnal analysis.

3.1. Fusion analysis

All fusion assessments (micro-CT and manual) conﬁrmed L4-L5 osseous fusion in 100% of the rats exposed to rhBMP-2 (groups C and D), whereas no osseous fusion was found in non-exposed groups A or B (Fig. 1).

3.2. Serial bone TV measurement by in vivo micro-CT

The study group TVs showed no signiﬁcant differences on day 0. The TVs of groups C and D markedly increased to a similar extent 2 weeks after surgery (245.4 ± 74.5 mm³ and 233.1 ± 95.9 mm³, respectively). However, subsequent TVs in rats exposed to rhBMP-2 differed dramatically in the presence or absence of PTH 1-34. The group D TV decreased over time until 12 weeks, while the group C TV continued to increase over this time-period. This resulted in a signiﬁcant lower TV in the PTH 1-34-treated group D at 12 weeks (180.4 ± 76.5 mm³), than in the control group C (323.5 ± 86.3 mm³) (p < 0.01; Fig. 2). Groups A and B showed a slight increase in TV 12 weeks after surgery, which...
may reflect age-related skeletal growth (group A: 73.3 ± 11.3 mm³; group B: 69.5 ± 10.2 mm³; p = 0.79).

The axial reconstructed images of rats exposed to rhBMP-2 clearly demonstrated that in the saline-treated group C, the contour of the fusion mass gradually enlarged between 2 and 12 weeks postoperatively, with little bone formation inside this mass. In contrast, the contour of the fusion mass apparently shrank between postoperative weeks 2 and 12 weeks in the PTH 1-34-treated group D, with robust new bone formation inside this mass (Fig. 3).

### 3.3. Microstructural indices of the newly formed bone

Groups C and D were used for this analysis because specimens from rats that were not exposed to rhBMP-2 (groups A and B) showed little or no new bone formation. PTH 1-34 administration significantly increased the trabecular BV, BV/TV, Tb.Th, and Tb.N, while the Tb.Sp significantly decreased. The cortical bone ratio (Sv/Av [%]) and average thickness (Ct [μm]) were also increased by PTH 1-34 administration, while the TV of the newly formed bone was significantly decreased (Table 2).

### 3.4. Effect of PTH administration on the adjacent vertebra (L6) and femur

The BV/TV values of both the distal femoral epiphysis and the L6 vertebral body were significantly increased by the administration of PTH 1-34, as compared to those observed in control rats (femur: 28.4 ± 10.7% vs. 61.4 ± 13.5%, p < 0.0001; L6 vertebra: 22.8 ± 10.6% vs. 44.0 ± 10.8%, p < 0.00001, respectively).

### 3.5. Serum bone metabolism markers

Significantly higher levels of osteocalcin (p < 0.001) and CTX-1 (p < 0.01) were observed in rats treated with PTH 1-34, as compared to the levels in rats treated with saline, whereas these groups showed no differences in the serum levels of P1NP or TRACP-5b (Fig. 4).

### 3.6. Histology

Microscopic evaluation of the coronal spinal sections showed that groups A and B showed minimal new bone formation, irrespective of PTH 1-34 administration (Fig. 5A and B), whereas those treated with rhBMP-2 (groups C and D) showed abundant new bone formation, bridging the transverse processes. The majority of the newly formed fusion mass in group C, which did not receive PTH 1-34, comprised fatty marrow within a large thin eggshell-like cortical bone (Fig. 5C). However, group D had a relatively small fusion mass that was filled with abundant trabecular bone (Fig. 5D).

### 3.7. Bone histomorphometry

The administration of PTH 1-34 significantly increased the MAR, dLS/BS, MS/BS, and N·Oc/BS of cancellous bone. This indicated that PTH 1-34 stimulated modeling and remodeling processes within 12 weeks of surgery (Table 3). Cortical bone histomorphometry demonstrated that PTH 1-34 administration significantly increased the bone resorption rate at the peristium and MAR at the endosteum. This treatment also tended to increase endosteum BFR/BS and sLs/BS, although this failed to achieve statistical significance (p = 0.08). These findings revealed predominant periosteal bone resorption and endosteal bone formation in PTH 1-34-treated rats (Figs. 6 and 7).

### 4. Discussion

The present study showed that intermittent administration of PTH 1-34 significantly decreased the TV of new rhBMP-2-induced bone, following the initial formation of a fusion mass equivalent to that of the

![Fig. 2. Serial tissue volume (TV) measurements of newly formed bone by in vivo micro-computed tomography are shown over the 12-week study in the indicated treatment groups. rhBMP-2, recombinant human bone morphogenetic protein; PTH 1-34 parathyroid hormone 1-34. **p < 0.01. TV is defined as a total bone tissue volume.](image)

![Fig. 3. Representative axial micro computed tomography images at postoperative weeks 2 and 12 are shown for the indicated study groups. rhBMP-2, recombinant human bone morphogenetic protein; PTH 1-34 parathyroid hormone 1-34. Arrows indicate shrinkage of the fusion mass in the groups treated with PTH 1-34.](image)
control group. Bone histomorphometry demonstrated predominant bone resorption at the periosteum and bone formation at the endosteum in rats receiving PTH 1-34. These results indicated that PTH 1-34 supported modeling of rhBMP-2-induced bone. Furthermore, the increased bone formation and bone resorption identified by bone histomorphometry and serum markers indicated that PTH 1-34 had a remodeling effect on rhBMP-2-induced bone; to definitely distinguish between modeling and remodeling, the systemic parameters of bone turnover were measured.

We believe that the decrease in the TV of the newly formed bone by PTH1-34 administration is interesting because the effects are applicable to the modeling process in fracture healing. The modeling effect by PTH1-34 enables spatial control of the excessively formed BMP-2-induced new bone possibly in response to the mechanical stress. The following three mechanisms may contribute to this accelerated bone modeling and remodeling. First, the combined administration of rhBMP-2 and PTH 1-34 produces a synergistic induction and differentiation of osteoblasts and osteoclasts in the rhBMP-2-induced fusion mass.

Fig. 4. Osteocalcin (bone formation marker) and type 1 collagen cross-linked C-telopeptides (CTX-1; bone resorption marker) significantly increased with the administration of teriparatide, but tartrate-resistant acid phosphatase (TRACP)-5b and N-terminal propeptide of type 1 procollagen (P1NP) levels were not significantly altered (n.s.). The double asterisk indicates $p < 0.0001$, the single asterisk indicates $p < 0.01$.

Table 3
Bone histomorphometric parameters of fusion mass.

| Parameters          | Saline      | PTH 1-34   |
|---------------------|-------------|------------|
| Cancellous bone     |             |            |
| OS/BS (%)           | 8.7 ± 5.0   | 13.2 ± 4.8 |
| ES/BS (%)           | 13.7 ± 4.7  | 13.4 ± 4.0 |
| N-Ob/BS (N/mm)      | 3.6 ± 1.6   | 7.2 ± 2.9  |
| N-Oc/BS (N/mm)      | 1.1 ± 0.4   | 2.0 ± 0.5* |
| MS/BS (%)           | 10.9 ± 6.3  | 22.1 ± 6.0 |
| MAR (μm/day)        | 1.0 ± 0.4   | 1.8 ± 0.2* |
| BFR/BS (mm²/mm²)    | 0.05 ± 0.05 | 0.15 ± 0.05* |
| BRR (mm³/mm²/yr)    | 0.02 ± 0.02 | 0.04 ± 0.02 |
| Cortical bone       |             |            |
| peristeum BFR/BS (mm²/mm²/yr) | 0.09 ± 0.14 | 0.34 ± 0.22 |
| BRS (mm³/mm²/yr)    | 0.13 ± 0.14 | 2.04 ± 1.45* |
| dls/BS (%)          | 11.1 ± 14.6 | 40.8 ± 25.9 |
| sLS/BS (%)          | 9.6 ± 6.0   | 9.6 ± 6.0  |
| MAR (μm/day)        | 5.6 ± 4.1   | 1.9 ± 0.3  |
| endosteum BFR/BS (mm²/mm²/yr) | 0.22 ± 0.11 | 0.42 ± 0.20 |
| BRS (mm³/mm²/yr)    | 0.33 ± 0.33 | 1.01 ± 1.30 |
| dls/BS (%)          | 36.5 ± 7.6  | 47.0 ± 19.4 |
| sLS/BS (%)          | 23.0 ± 15.8 | 11.1 ± 2.9 |
| MAR (μm/day)        | 1.2 ± 0.4   | 2.1 ± 0.5* |

Values are given as the mean and standard deviation. BFR/BS, bone formation rate; BRS, bone resorption rate; dls/BS, double-labeled surface; ES/BS, eroded surface; N.Ob/BS, MAR, mineral apposition rate; MS/BS, mineralizing surface; osteoblast number; N.Oc/BS, osteoclast number; OS/BS, osteoid surface; sLS/BS, single-labeled surface; PTH: parathyroid hormone.

* The value was significantly higher in the group that received PTH 1-34 ($p < 0.05$).

Fig. 5. Lower-power photomicrographs of coronal sections of the L4-5 transverse spine processes are shown for rats in the indicated study groups (A–D) at a magnification of ×0.5. See Table 1 for a description of the study group treatments.
these effects. (1) PTH 1-34 stimulates T-cell production of the osteogenic Wnt ligand, Wnt10b, which stimulates bone formation by osteoblasts (Baron and Kneissel, 2013). (2) BMP signaling upregulates the expression of SOST, leading to the increased translation of sclerostin, which negatively regulates the Wnt pathway (Kamiya et al., 2008). PTH 1-34 inhibits osteocyte sclerostin expression and activates Wnt signaling (Fermor and Skerry, 1995), which promotes the differentiation of mesenchymal stem cells to osteoblasts, rather than adipocytes (Takada et al., 2009). Indeed, we found that the newly formed bone was filled with adipose tissue in rats exposed to rhBMP-2 without PTH 1-34. (3) PTH stimulates the endocytosis of the BMP antagonist, thus enhancing BMP signaling by blocking the negative influence of BMP antagonists, including noggin (Yu et al., 2012). (4) The osteoblasts induced by the above pathways also recruit and differentiate osteoclasts by expressing receptor activator of nuclear factor kappa-B ligand (RANKL) (Nakashima et al., 2011).

Second, PTH 1-34 has a unique mechanism of action in bone whereby intermittent administration leads to a rapid increase in bone formation markers, followed by an increase in bone resorption markers (Canalis, 2010; Canalis et al., 2007; Jilka, 2007; Manabe et al., 2007; Tam et al., 1982). The present study demonstrated that markers of both bone formation and resorption significantly increased in the PTH 1-34-treated group 12 weeks after surgery. A high bone turnover, with predominant bone formation by osteoblasts, can promote bone.
modeling and remodeling. The obvious osteon structure visible using polarization microscopy also confirmed the accelerated remodeling in the rhBMP-2-induced bone in rats treated with PTH 1-34 (Fig. 6, E).

Third, recent studies suggest that osteocyte PTH/PTH-related peptide type 1 receptor signaling regulates anabolic and catabolic skeletal responses to PTH (Saini et al., 2013). Osteocytes, the most abundant cells in bone, have recently emerged as important modulators of bone modeling (Maycas et al., 2015; Saini et al., 2013; Zhang et al., 2009). During normal physiological skeletal growth, bone modeling involves bone formation at the periosteum and bone resorption at the endosteum. However, in pathological situations, such as angulated long bone malunions in children or fracture healing, diverse patterns of bone architecture modeling occur in response to mechanical stress; these include predominant periosteal bone resorption and endosteal bone formation. PTH has profound effects on cortical bone, stimulating periosteal expansion and accelerating intracortical bone remodeling by activating osteocyte PTH receptors during normal bone modeling (Rhee et al., 2011). Intermittent PTH administration stimulates osteocyte-mediated modeling in response to mechanical stress through connexin 43 and osteocyte-mediated RANKL expression (Pacheco-Costa et al., 2015). These mechanisms might play a role in the modeling and remodeling of rhBMP-2-induced bone by PTH 1-34. All these data suggest that concomitant administration of PTH 1-34 and rhBMP-2 could promote the production of high-quality bone, and also promote the modeling and remodeling of newly formed bone in response to mechanical requirements (Komatsubara et al., 2005).

This study has several limitations. We employed only one dose of rhBMP-2 (50 μg), although we previously tested 2 μg and 50 μg rhBMP-2. We anticipated that it would be difficult to compare the effects of PTH 1-34 on modeling and remodeling in a 2 μg rhBMP-2 group because the fusion rates were previously around 50% in this group and pseudoarthrosis would affect the fusion rates. A further limitation is that the current spinal fusion model in quadrupedal rodents cannot be directly extrapolated to spinal arthrodesis in humans because of the differences in biomechanics and biological effects of the agents. Another limitation is the lack of a biomechanical assessment of fusion because of the size and complex geometry of the rat spine. However, in this study, 100% fusion was observed in the rhBMP-2-treated rats and the microstructural indices derived using micro-CT were previously reported to correlate with biomechanical properties (Leahy et al., 2010). Another limitation is the lack of verification of influence of mechanical stress on the PTH1-34 related modeling effect. In this model of spinal fusion, it is difficult to inhibit the effect of mechanical stress by external fixation or other methods. A study using the femoral defect model combined with plate fixation is underway. The results from the study will further clarify the relationship between the modeling effect of PTH1-34 and mechanical stress. In conclusion, the present study demonstrated that intermittent PTH 1-34 administration significantly accelerated the modeling (volume reduction) of rhBMP-2-induced new bone and significantly improved the quality of the newly formed bone by accelerating remodeling. Our results indicate that the combined administration of rhBMP-2 and PTH 1-34 may enable the spatial control of newly formed bone in the presence of mechanical stress.

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