Local anti-inflammatory effect and immunomodulatory activity of chitosan-based dressing in skin wound healing: A systematic review

Karla C. Maita, Francisco R. Avila, Ricardo A. Torres-Guzman, John P. Garcia, Abdullah S. Eldaly, Luiza Palmieri, Omar S. Emam, Olivia Ho, Antonio J. Forte*
Division of Plastic Surgery, Mayo Clinic, Jacksonville, Florida, USA

ABSTRACT

Background and Aim: Wound healing is a complex process comprised of several distinct phases. An imbalance in any of the stages creates a chronic wound with the potential to cause life-threatening complications for patients. Chitosan (CS) is a biopolymer that has shown to positively impact the different healing phases. This systematic review aimed to evaluate the anti-inflammatory and immunomodulatory properties of CS-based wound therapy for the skin healing process after an injury.

Methods: A systematic review was conducted in November 2021 following the Preferred Reporting Items for Systematic Reviews and Meta-analyses guidelines. The PubMed, Embase, Google Scholar, and Cochrane online databases were queried to capture all publications in the past 10 years that investigated the CS effects on inflammation and immune reaction.

Results: A total of 234 studies were screened after removing duplicates and 14 articles fulfilled our inclusion and exclusion criteria. In the studies, CS was combined with a wide range of products. One clinical trial was found that treated patients with diabetic foot ulcers. All animal models in the studies used a full-thickness skin wound to test the effectiveness of CS in the healing process. Decreased pro-inflammatory cytokine levels, a shortened inflammatory phase and accelerated wound closure was observed in all of the studies.

Conclusions: CS proved to be a feasible, versatile, and multifaceted biomaterial that enhances the biological response to a skin injury. When combined with other products, its potential to boost the healing process through regulation of the inflammatory and cellular activity is increased.

Relevance for Patients: Although few clinical trials have been completed, CS has become an excellent alternative to modulate the local inflammatory response promoting wound healing. Especially in patients with associated comorbidities that affect the typical resolution of skin healing, such as diabetes and vascular insufficiency. Therefore, using bioactive wound dressings based on CS combined with nanoparticles, growth factors, lived cells, or medications released in a controlled manner positively impacts patient life by shorting the wound healing process.

1. Introduction

The skin is the largest organ in the body and has the capacity to regenerate itself [1]. After an injury, the skin heals through several phases called hemostasis, inflammation, proliferation, and remodeling (Figure 1) [2,3]. Although the skin can return to a normal state and regain its regular function, a series of factors, such as infection, foreign body presence, tissue necrosis, and patient comorbidities, can disrupt its healing [4,5]. Therefore, a delay in wound closure increases the risk of bacterial colonization, invasion, and sepsis instauration leading patients to a life-threatening conditions [6,7].

DOI: http://dx.doi.org/10.18053/jctres.08.202206.007
In the United States alone, the health-care system spends more than $70 billion on wound care each year [8-10]. Thus, it is necessary to find an effective treatment option that boosts the natural skin healing process by regulating the cytokines and growth factors that play a crucial role in modulating the cellular activity at the injury site [11]. Chitosan (CS) is a naturally derived biopolymer from the crustaceous cytoskeleton [12-14], and it has previously shown to improve different phases of the skin healing process [15-18]. Important properties for tissue regeneration associated with this biomaterial include antimicrobial and anti-inflammatory activity, angiogenesis promotion, and collagen synthesis stimulation [19-23]. These properties have been potentiated by adding substances, chemicals components, and active biomolecules [24-26]. Accordingly, antioxidant properties have been found by combining CS with hyaluronan and phosphatidylcholine dihydroquercetin. Considering that the excessive production of free radicals during the inflammatory phase of healing exerts a negative effect on the cellular performance during the immune response, enhancing the elimination of the free radicals from the wound will decrease inflammation and promote skin regeneration [27].

Immune response modulation at the skin injury site shortens the healing course by decreasing pro-inflammatory cytokine production, neutrophil infiltration, and number of reactive oxygen species while increasing specific growth factors that favor skin regeneration [2,28-30]. Furthermore, finding the perfect balance between cytokines and chemokines production in the inflammatory stage of skin healing will orchestrate the interaction between platelets, neutrophils, macrophages, and monocytes essential for a successful recovery [3,31].

We hypothesize that CS can regulate the immune response and decrease inflammation at the wound site, thus enhancing the skin healing process. This systematic review evaluates the anti-inflammatory and immunomodulatory properties of different forms of CS for skin regeneration after an injury.

2. Methods
2.1. Study selection

A systematic review of articles illustrating skin wound healing using CS in in-vivo models was performed. The Preferred Reporting Items for Systematic Reviews and Meta-analyses (PRISMA) guidelines were followed for article identification and final selection [32]. Papers written in English that reported the utilization of the CS biomaterial, alone or in combination, to treat wounds were included in the study. In addition, assessment of the CS’s anti-inflammatory activity through histological or molecular analysis or gene expression quantification associated with skin healing process was required for inclusion. On the other hand, studies were excluded if they described in vitro or in vivo models with only macroscopy or gross morphological evaluation of the wounds.

2.2. Data source and search strategy

The search was conducted on November 18, 2021, by querying the electronic databases MEDLINE (PubMed), EMBASE, Google Scholar, and Cochrane Central Register of Controlled Trials. We used a combination of the following Medical Subject Headings terms: “Anti-inflammatory activity” AND “chitosan” AND “skin wound healing”. The inquiry was limited to articles published in the past 10 years. Assessment of the studies’ titles and abstracts constituted the initial screening. For the final selection, a comprehensive literature review referring to the inclusion and exclusion criteria described above was completed. Two authors independently performed the search and an agreement among them was attained.
2.3. Risk of bias

The Risk of Bias in Non-Randomized Studies – of Interventions tool (Cochrane Library) was used to evaluate studies’ risk of bias [33]. Descriptions of individualized bias and cross-sectional studies bias are shown in Figures 2 and 3, respectively.

3. Results and Discussion

3.1. Study selection and principal characteristics

The study selection process is outlined in the PRISMA flow diagram (Figure 4). Out of the 234 articles identified initially, a total of 14 articles fulfilled the inclusion criteria. A summary of the important characteristics of each article is presented in Tables 1 and 2.

Thirteen of the studies utilized animal models with more than 50% of them examining rats as the main species [26,34-40], followed by mice [41-45]. A single paper reported a double-blind, randomized, and clinical trial with humans to assess the use of CS combined with isosorbide dinitrate to treat diabetic foot ulcers [46].

A variety of CS forms were described, including hydrogels [41-44,46], sponges [34], membranes [26], dressings [39,40], patches [38], nanoparticles (NP) [37], and scaffolds [35,36,45]. No application of CS alone was reported. Collagen [35,36,41], alginate [39], hyaluronan [26], curcumin [36,37], platelet-rich plasma [40], metal ions [44], human dermal fibroblast [34], and growth factors [42,43] were combined with the CS to improve the healing process. A full-thickness cutaneous wound on the dorsum of the animal was created as the injury for all the animal models. In addition, some studies assessed the association of comorbidities in the skin regeneration by producing skin radiation lesions [34], inducing diabetes [37,41,42], and coinfecting the wound [40]. Similarly, the benefits of CS on chronic wounds were evaluated in diabetic patients with foot ulcers. Sutto et al. [46] achieved complete foot ulcer closure in 68 diabetic patients in fewer days when CS was combined with isosorbide nitrate compared to CS alone or a placebo.

3.2. Inflammatory and angiogenesis mediators in the skin healing process

Hemostasis and inflammation are the initial steps of skin healing and occur within the first 3 days after an injury [31,47]. Neutrophils are the most abundant white blood cells at the wound site during the first 24 h [47]. Their recruitment is mediated by pro-inflammatory cytokines, such as interleukin (IL)-1, IL-6, Interferon (IFN)-α, tumor necrosis factor (TNF)–α, transforming growth factor (TGF)–β, macrophage inflammatory protein-1α, and anaphylatoxins (C3a, C5a). However, IL-6 secreted mainly by macrophages, endothelial cells, and fibroblasts has been described as one of the principal regulators in neutrophil recruitment [48]. High levels of IL-6 are related to poor wound healing and scarring [49].

Li et al. [37] analyzed the performance of the Curcumin (Cur) and CS NPs in an in vitro model, an lower expression of NF-kB and downregulation of TNF-α and IL-6 were observed. This demonstrated that Cur-CS-NPs inhibited the macrophage-induced inflammatory response. To test these results, wounds of diabetic rats were treated with Cur-CS-NPs. Thus, less inflammatory cellular infiltration, increased the production of new blood vessels, and a superior collagen distribution were found in the experimental group.

Comparable results were reported by Hu et al. [42]. They found a decrease in levels of IL-6 when wounds of streptozotocin-induced diabetic mice were treated with CS hydrogel combined with Cur-NPs, aldehyde hyaluronic acid, carboxymethyl, and epithelial growth factor compared to the control group. Furthermore, the implementation of this hydrogel allowed a controlled release of the components throughout the healing process. Thus, it was demonstrated that CNPs assuaged oxidative stress and inflammation during the early stage, while the late secretion of EGF drove the extracellular matrix (ECM) remodeling. In
Table 1. Characteristics of included clinical trials

| Author/Year/Location | Number of patients | Type of study | Chitosan form | Combination loaded | Control group | Type of injury | Time of healing | Histology | IHC |
|----------------------|--------------------|---------------|---------------|-------------------|---------------|---------------|----------------|-----------|-----|
| Sutto et al. (2018) Mexico | 68 | Randomized Placebo-controlled Double-blinded Clinical trial | Gel | Isosorbide Dinitrate | Placebo | DFU | 30 days | TG 45 days | Placebo |

α-SMA: α-smooth muscle actin, DFU, diabetic foot ulcers, IHC, immunohistochemistry, TG, treated group, VEGF-A, vascular endothelial growth factor-A, vWF, Von Willebrand factor.

Figure 4. Included and excluded studies following the Preferred Reporting Items for Systematic Review and Meta-analyses (PRISMA) flow diagram.

addition, the histopathological analysis of the wound tissue showed a faster granulation tissue formation, reepithelization, and hair follicle regeneration in the experimental group.

Anti-inflammatory properties of Cur-CS were as well tested by Rezaii et al. [36]. A Cur-CS-collagen scaffold was used to treat wounds in a rat model, and the team focused their investigation on TGF-β1 as this peptide has a broad range of effects on growth factors implicated in wound healing [31]. The histological analysis illustrated that the upregulation of TGF-β1 at the early and late stages of skin healing was associated with quicker wound closure, neovascularization, greater collagen content, and reepithelization.

In the presence of infection, neutrophils assist in combating bacterial invasion by releasing reactive oxygen species, cytotoxic granules, and increasing pro-inflammatory macrophages and T cell chemotaxis [50]. Hence, an increase in the quantity of neutrophils will prolong the inflammatory state [51]. Zhou et al. [40] created an infected wound through inoculation of Staphylococcus aureus and Escherichia coli in a full-thickness
### Table 2. Characteristics of included studies in animal models

| Author/Year/Location | Type of animal | Chitosan form | Combination loaded | Control group | Type of injury | Endpoint (Days) | Histology | IHC/IF/RT-qPCR/WBT |
|----------------------|----------------|---------------|-------------------|---------------|----------------|----------------|-----------|---------------------|
| Hilmi et al. (2013) Malaysia | Sprague-Dawley rats | Sponge (Dermal substitute) | Fibroblast | Duoderm CGF | Post-radiation injury (2 months) Full thickness cutaneous wounds 1 cm×1 cm | 7, 14, 21 | H&E MT distance ET length Re-epit | IF HLA K10 |
| You et al. (2017) China | Sprague-Dawley rats | Scaffold (NAg-CCS) | BT-1C MNAg 20–40nm in diameter | CCS | Full thickness skin defects in 2 cm Ø | 7, 14, 28 | H&E Fibroblast’s migration ECM MTS | IHC CD68 TGF-β1 RT-qPCR TNF-α TGF-β IL-10 IL-6 IFN-γ N/A |
| Tamer et al. (2018) Egypt | Wistar rats | Membrane Hyaluronan Edaravone Cotton gauze | Full thickness skin defects 1.5 cm×1.5 cm | 7, 14, 21 | H&E • Epithelialization area • Granulation tissue • Connective tissue | RT-qPCR TGF-β1 Smad7 |
| Rezaei et al. (2019) Tehran | Wistar rats | Scaffold CNs Collagen (-) Untreated (+) CCS | Full thickness cutaneous wounds 1 cm Ø | 3, 7, 15 | H&E • Epidermal thickness • Granulation tissue • Vascular density | MTS H&E • Inflammatory infiltrates • Neo-vascularization | N/A |
| Li et al. (2019) China | Sprague-Dawley rats Streptozotocin-induced diabetic rat models | Nanoparticles CNs PBS | Full thickness skin defects 2 cm Ø | 3, 7, 14 | H&E • Inflammatory infiltrates • Re-epi. • Granulation tissue | MTS HPA • Inflammatory infiltrates • Blood vessels • Fibroblasts | IL-6 N/A |
| Niranjan et al. (2019) India | Wistar rats | Patch CNs PVA (-) Untreated (+) Commercial ointment (mupirocin) | Full thickness skin defects 1.5 cm×1.5 cm | H&E • Inflammatory infiltrates • Re-epi. • Granulation tissue | MTS HPA | IHC IL-6 VEGF CD34 TGF-β1, Phospho-Smad2 Phospho-Smad3 IF Collagen I CD31 CD68 F4/80 ELISA TNF-α IL-6 IL-10 IL-4 IL-1β RT-qPCR Peritoneal macrophages |
| Zhao et al. (2020) China | Sprague-Dawley rats | Dressing CA | CAD | Full thickness wound model 2 cm Ø | 3, 7, 14 | H&E • Inflammatory infiltrates • Blood vessels • Fibroblasts | MTS | N/A |
| Shen et al. (2020) China | C57BL/6 mice Streptozotocin-induced diabetic mice models | Hydrogel scaffold Col I (-) Tegaderm (+) Col I | Full thickness wounds 8 mm Ø | 3, 7, 14, 18 | H&E • Re-epi. • Collagen deposition, • Epithelial thickness • Neo-vascularization | N/A | (Contd...) |
Table 2. (Continued)

| Author/ Year/ Location | Type of animal | Chitosan form | Combination loaded | Control group | Type of injury | Endpoint (Days) | Histology | HIC/IF/ RT-qPCR/ WBT |
|------------------------|----------------|---------------|-------------------|---------------|---------------|----------------|-----------|---------------------|
| Hu et al. (2021). USA  | C57BL/6 mice   | Hydrogel      | OHA CNs EGF       | Blank hydrogel OHA-CMC OHA-CMC/CNs OHA-CMC/EGF OHA-CMC/CNs/EGF | Fullthickness skin 8 mm Ø | 5, 10, 15 | H&E • Re-epi. • Granulation tissue • Neo-vascularization TS | HIC/IF IL-6 Collagen-I MMP9 CD31 |
| Li et al. (2020). China| Vegfr2-luc transgenic mice | Hydrogel | IGF-1 | PBS CS hydrogel CS–IGF-1C | Full-thickness wound 1 cm Ø | 3, 7, 14 | H&E • Neo-vascularization • ECM remodeling | IF CD31 Ki-67 RT-qPCR VEGFA HIF-1α PDGF ANG1 HIC Cytokeratine IF CD31 α-SMA TNF-α N/A |
| Xiao et al. (2021). China | C57BL/6 mice | Hydrogel | Metal Ions Ag⁺, Zn²⁺, and Cu²⁺ | Untreated CS alone coated gauze MD gauze | Full thickness cutaneous wounds 6 mm Ø | 7, 17 | H&E • Granulation tissue MTS | H&E • Angiogenesis • Inflammatory infiltrates | |
| Hashemikia et al. (2021). Iran | Balb/C mice | Scaffold | PEO Silica Ciprofloxacin nanofibers | Untreated CS/PEO CSPEO/SiO2 Chit/PEO/SiO2/ Cip | Full thickness excisional wound 6 mm Ø | 4, 7, 14 | H&E • Angiogenesis • Inflammatory infiltrates | N/A |
| Zhou et al. (2021). China | Sprague-Dawley rats | Dressing | Platelet rich plasma Sodium alginate (Alg) Silver (Ag) PAMAM | Gauze (-) Aquacel Ag (+) | Full thickness excisional wound Escherichia coli and Staphylococcus aureus co-infected | 7, 14 | H&E • Inflammatory infiltrates • Re-epi. MTS | HIC CD31 α-SMA, TNF-α IL-1β IL-6 TGF-β1 RT-qPCR CD31 α-SMA TGF-β TNF-a IL-6 IL-1β |

Ag⁺: Silver, Alg: Sodium alginate, ANG1: Angiopoietin 1, BT-1C: Bovine type 1 collagen, CA: Calcium alginate, CAD: Calcium alginate dressing, CS: Chitosan, CNs: Curcumin nanoparticles, CMC: Carboxymethyl chitosan, Cu²⁺: Copper, EGF: Epidermal growth factor, ECM: Extracellular matrix, ET: Epithelial tongue, HIF-1α: Hypoxia inducible factor 1 alpha, H&E: Hematoxylin and eosin, hDF: Human dermis fibroblast, IFN-γ: Interferon gamma, IGF-1C: Insulin growth factor 1C, IHC: Immunohistochemistry, IF: Immunofluorescence, IL: Interleukin, MD: Multi XX, MMP9: Metalloprotease 9, MNAg: Metallic nano silver particles, MT: Migratory tongue, MTS: Masson’s trichrome staining, N/A, Not applicable, OH: Aldehyde hyaluronic acid, PAMAM: Polyamido amine, PBS, Phosphate-buffered saline, PDGF: platelet-derived growth factor, POE: Polyethylene oxide, Re-epi: Re-epithelization, RT-qPCR: Real time quantitative polymerase reaction chain, SiO₂: Silica, TGF-β: Transforming growth factor beta, TNF-α: Tumor necrosis factor alpha, WBT: Western blood test, Zn²⁺: Zinc.

Skin lesion in rats. The group tested the healing properties of a nanosilver-doped carboxymethyl CS-grafted polyamide amine cationic polymer dressing mixed with platelet-rich plasma and sodium alginate (Alg/Ag@CMC-PAMAM/Platelet rich plasma [PRP]). The downregulation of IL-6 and IL-1β and the up-regulation of TGF-β, CD31, and α-SMA in the rats treated with the dressing demonstrated that Alg/Ag@CMC-PAMAM/PRP supports healing of infected wounds by increasing angiogenesis and decreasing inflammation.

Similarly, You et al. [35], evaluated the in vitro anti-microbial properties of a collagen-CS-based scaffold combined with silver nanoparticles (NAg-CCs). Different concentrations of NAg were tested against E. coli and S. aureus, and the minimal inhibitory concentration was found to be ≤10 ppm. Therefore, they fabricated NAg-CCs scaffolds with this concentration, and the in vivo performance was studied. Afterward, real-time quantitative polymerase chain reaction (RT-qPCR) was used to assess the anti-inflammatory activity. A significantly lower mRNA...
expression of IL-6, TNF-α, and TGF-β in the NAg-CCs group was detected compared to the control group that contained CS alone. In addition, overexpression of IL-10 and IFN-γ was found at 1, 2, and 4 weeks after scaffold implantation. A western blot analysis supported these results at each time point.

Metal ions constitute another essential component of the wound microenvironment and their presence is crucial for cellular biochemistry reactions. Some of the most studied metal ions and their function on skin healing include silver (Ag⁺) which is recognized as an excellent option to treat infected wounds [39,52]; calcium (Ca²⁺) related to improving reepithelization [53]; zinc (Zn²⁺) associated with immune response, cell growth and migration [54]; and copper (Cu²⁺) distinguished as a collagen stabilizer and angiogenesis promoter [55]. Based on these promising metals properties, Xiao et al. [44] created a gauze base dressing with CS hydrogel to load metal ions (Ag⁺, Ca²⁺, Zn²⁺, Cu²⁺) to treat S. aureus infected wounds. The freeze-thawing was the method used to create multiple ions coloaded gauze (MD), layer-by-layer gauze (LBL), and timely dosing gauze (TD). LBL and TD can release multiple metal ions on demand in an in vitro model. The dressings’ anti-inflammatory properties were assessed on day 7 through immunofluorescence staining of the tissue. This showed a down-regulation of the TNF-α pro-inflammatory cytokine in all groups except in CS group. Furthermore, the growth pattern of bacterial colonies was documented. The MD and LBL groups showed significant colony reduction in the first 2 days compared to the TD group, which had the best anti-bacterial activity on day 7. Therefore, metal ions integrated into a gauze delayed bacterial growth in vitro and inhibited inflammation in vivo through TNF-α regulation and macrophage polarization. This ion delivery system proved to have an excellent anti-bacterial action and can be an option for infected wound treatment.

In addition to the angiogenic properties of CS proven by Zhou et al., [40] using Alg/Ag@CMC-PAMAM/PRP on infected wounds, Zhao et al. [39] observed an increase in neovascularization molecules related to VEGF and CD31 in an animal model. They fabricated fibrous spongiform calcium alginate (CAD) dressing mixed with CS (CCAD) to treat full-thickness wounds. More blood vessels and faster healing were reported in the CCAD group compared to the CAD group. The anti-inflammatory activity was additionally evaluated through the IHC staining of IL-6, and the CCAD group had lower IL-6 levels.

Li et al. [43] demonstrated the capability of CS hydrogel to carry growth factors to promote wound healing. Angiogenesis was increased after applying a CS-IGF-1C hydrogel in vegf2-transgenic mice. Bioluminescence confirmed the activation of the VEGF/VEGFR2 pathway. In addition, the levels of the proangiogenic genes (VEGF-A, HIF-1α, ANG1, and PDGF) were determined and they were significantly higher in mice treated with the CS-IGF-1C hydrogel. Moreover, Wang et al. [56] proved the practicality of this hydrogel by combining it with hyaluronic acid and adipose-derived stromal cells. The cotransplantation of the hydrogel and stem cells into the ischemic hind limbs of mice effectively increased blood perfusion and decreased inflammation.

3.3. The importance of balancing macrophage activation in the skin inflammatory response

Macrophages are widely described as a necessary for skin regeneration. Its depletion results in a reduction of ECM formation and angiogenesis leading to delayed wound closure [57]. Two identified subsets of skin macrophages exist. One is known as the resident macrophages and the other is the circulating monocyte-derived macrophages. The latter plays the central role in skin healing as the resident macrophages only provide a short-term response to an injury [58].

Once monocytes arrive at the wound site, they differentiate into two critical types of monocyte-derived macrophages, M1 (proinflammatory) and M2 (reparative) (Figure 5). In normal conditions, 80–85% of the M1 macrophages transitioned into M2 macrophages around day 5–7 post-injury. This is characterized by the production of cytokines (IL-4, IL-10, and IL-13) and growth factors (VEGF, TGF-β, PDGF, and IGF-1) that promote proliferation of keratinocytes, fibroblasts, and endothelial cells that lead to reepithelization and generate ECM components [59]. Therefore, dysregulation of these subtypes of macrophages results in non-healed wounds or tissue fibrosis [57]. Shen et al. [41] demonstrated that the macrophage immune response modulation occurred when using a sulfated CS doped collagen Type I (Col I/SCS) hydrogel for diabetic mouse wound treatment. Induction of polarization toward the M2 subpopulation (CD206⁺) enhanced the macrophages’ trans-differentiation into fibroblasts. Similarly, the use of NAg-CCs scaffold produced regulation of fibroblast migration and macrophage activation in the injury site demonstrated by low expression of CD68, TGF-β, and IL-6 and a high expression of IL-10 and IFN-γ. Importantly, IFN-γ is a known inducer of the M2 macrophages [35,57]. Comparably, CNs were incorporated into a CCs scaffold. Modulation of TGF-β1 and Smad7 levels was observed. The up-regulation of TGF-β1 mRNA on days 3 and 15 and Smad7 mRNA on day 5 post-treatment demonstrated negative feedback between these two molecules. This relationship contributed to rapid wound closure due to accelerated progression from the inflammatory to the proliferative healing phase [36].

On the other hand, a higher M2/M1 ratio was observed in wounds treated with CS metal ion-loaded gauzes. An increase in M2 phenotype demonstrated that the host’s immune response could be modulated using drugs, preventing pathological macrophage activation [44]. The association of dysfunctional macrophages with the development of chronic wounds has been observed in diabetic patients [57,59]. Targeting macrophages directly through a therapeutic intervention may enhance wound healing. Using Col I/SCS hydrogel on diabetic mice, Shen et al. [41] observed an up-regulation of IL-4 promoting macrophage polarization into the M2 phenotype. These results are comparable to those reported by Bonito et al., [60] and Schirmer et al. [61], which highlight the role of IL-4 in the modulation of macrophage activation. In addition, Col I/SCS increased transdifferentiation of macrophages into fibroblasts, expanding the synthesis of ECM components and improving wound healing [41].
3.4. Histopathological analysis

The therapeutic effect of CS in combination with several products was tested in 13 of the 14 studies by performing a morphological tissue evaluation using hematoxylin and eosin staining. A decrease in the inflammatory cells infiltration [37,38,40,45,59] and the balance in granulation tissue formation [26,36,38,42,44] were reported by the majority of the authors. In addition, it described was an increase in reepithelization [26,34,36,38,40-42], and neovascularization [36,37,39,41-43,45,46].

Hydroxyproline content in the wounds was determined by Niranjan et al. [38] to evaluate the ECM formation capacity of polyvinyl alcohol/CS/curcumin patches. Higher content was observed in the group treated with the patches compared to the group managed with a commercial ointment. In addition, the skin samples assessed collagen deposition by Masson Trichrome staining. On the 16th day post-treatment, the tissue samples showed thickness, dense, and uniform collagen fibers. These results were similar to those reported by studies using CS combined with collagen/silver [35], collagen/curcumin [36], calcium alginate [39], sodium alginate/PRP/silver/PAMAM [40], and hyaluronic acid/curcumin/EGF [42]. The surge of tissue-engineered materials has allowed the creation of bioactive wound dressings to boost lesion healing [12]. CS has demonstrated versatility in this field due to its use in various forms, such as sponges, patches, membranes, scaffolds, and hydrogels. Moreover, the inclusion of NP, growth factors, lived cells or medications, and released in a controlled manner further increases its usefulness for skin healing.

3.5. Limitation

The main limitation of this study was the discrepancies found between studies discussing CS in combination with several components as it was challenging to compare them. In addition, the diversity of the protocols employed in the reviewed studies can contribute to the potential misinterpretation of data and results. Finally, the study selection process of systematic reviews may be a source of bias.

4. Conclusions

The skin begins a cascade of events following an injury, with inflammation being one of the most determining factors in healing. Hence, several therapeutic options focus on controlling this stage to accelerate wound closure. CS has shown to decrease inflammation, promote neovascularization, reepithelization, and prevent bacterial infiltration at the wound site in in vivo models. Its capacity to be combined with a variety of products known to promote wound healing, exerting a synergistic effect, demonstrates its versatility as a biomaterial. Therefore, with CS being inexpensive and accessible, it can provide a feasible alternative as a therapeutic option for wound treatment.

Acknowledgments

None.

Funding

This study was supported in part by the Mayo Clinic Clinical Research Operations Group and Mayo Clinic Center for Regenerative Medicine.

Conflicts of Interest

None.

References

[1] Swann G. The Skin is the Body’s Largest Organ. J Vis Commun Med 2010;33:148-9.
[2] Rodrigues M, Kosaric N, Bonham CA, Gurtner GC. Wound Healing: A Cellular Perspective. Physiol Rev 2019;99:665-706.
[3] Gurtner GC, Werner S, Barrandon Y, Longaker MT. Wound Repair and Regeneration. Nature 2008;453:314-21.

[4] Falanga V. Wound Healing and its Impairment in the Diabetic Foot. Lancet 2005;366:1736-43.

[5] Han G, Ceilley R. Chronic Wound Healing: A Review of Current Management and Treatments. Adv Ther 2017;34:599-610.

[6] Lemsanni M, Najeb Z, Zoukal S, Chafik R, Madhar M, Elhaoury H. Necrotizing Fasciitis of the Upper Extremity: A Retrospective Analysis of 19 Cases. Hand Surg Rehabil 2021;40:505-12.

[7] Soh EZ. Necrotizing Soft Tissue Infection of Left Shoulder and Upper Limb Following Intravenous Injection of Non-steroidal Anti-inflammatory Drug. Cureus 2021;13:e18068.

[8] Fife CE, Carter MJ. Wound Care Outcomes and Associated Cost Among Patients Treated in US Outpatient Wound Centers: Data From the US Wound Registry. Wounds 2012;24:10-7.

[9] Dillingham TR, Pezzin LE, Shore AD. Reamputation, Mortality, and Health Care Costs Among Persons with Dysvascular Lower-limb Amputations. Arch Phys Med Rehabil 2005;86:480-6.

[10] Sen CK. Human Wound and its Burden: Updated 2020 Compendium of Estimates. Adv Wound Care (New Rochelle) 2021;10:281-92.

[11] Finnson KW, McLean S, Di Guglielmo GM, Philip A. Dynamics of Transforming Growth Factor Beta Signaling in Wound Healing and Scarring. Adv Wound Care (New Rochelle) 2013;2:195-214.

[12] Kim IY, Seo SJ, Moon HS, Yoo MK, Park IY, Kim BC, et al. Chitosan and its Derivatives for Tissue Engineering Applications. Biotechnol Adv 2008;26:1-21.

[13] Muzzarelli RA, Mattioli-Belmonte M, Pugnaloni A, Biagini G. Biochemistry, Histology and Clinical uses of Chitins and Chitosans in Wound Healing. EXS 1999;87:251-64.

[14] Shivakumar P, Gupta MS, Jayakumar R, Gowda DV. Prospection of Chitosan and its Derivatives in Wound Healing: Proof of Patent Analysis (2010-2020). Int J Biol Macromol 2017;184:701-12.

[15] Amin MA, Abdel-Raheem IT. Accelerated Wound Healing and Anti-inflammatory Effects of Physically Cross Linked Polyvinyl Alcohol-chitosan Hydrogel Containing Honey Bee Venom in Diabetic Rats. Arch Pharm Res 2013;8:1-16.

[16] Amin MA, Abdel-Raheem IT, Madkor HR. Wound Healing and Anti-inflammatory Activities of Bee Venom-chitosan Blend Films. J Drug Delive Sci Technol 2008;18:424-30.

[17] Chi J, Zhang X, Chen C, Shao C, Zhao Y, Wang Y. Antibacterial and Angiogenic Chitosan Microneedle Array Patch for Promoting Wound Healing. Bioactive Mater 2020;5:253-9.

[18] Halim AS, Nor FM, Saad AZ, Nasir NA, Norsa’adah B, Ujang Z. Efficacy of Chitosan Derivative Films Versus Hydrocolloid Dressing on Superficial Wounds. J Taibah Univ Med Sci 2018;13:512-20.

[19] A.S. Harti, S. Dwi Sulisetyawati, A. Murharyati, M. Oktariani, I.B. Wijayanti, The effectiveness of snail slime and chitosan in wound healing, International Journal of Pharma Medicine and Biological Sciences 5(1) (2016) 76-80.

[20] Huber D, Grzelak A, Baumann M, Borth N, Schleining G, Nyanhongo GS, et al. Anti-Inflammatory and Anti-oxidant Properties of Laccase-synthesized Phenolic-O-carboxymethyl Chitosan Hydrogels. New Biotechnol 2018;40:236-44.

[21] Kim S. Competitive Biological Activities of Chitosan and its Derivatives: Antimicrobial, Antioxidant, Anticancer, and Anti-inflammatory Activities. Int J Polym Sci 2018;2018:1708172.

[22] Hassan MA, Omer AM, Abbas E, Baset WM, Tamer TM. Preparation, Physicochemical Characterization and Antimicrobial Activities of Novel Two Phenolic Chitosan Schiff Base Derivatives. Sci Rep 2018;8:111416.

[23] Yilmaz E. Chitosan: A Versatile Biomaterial. Adv Exp Med Biol 2004;553:59-68.

[24] Costain DJ, Kennedy R, Ciona C, McAlister VC, Lee TD. Prevention of Postsurgical Adhesions with N,O-carboxymethyl Chitosan: Examination of the Most Efficacious Preparation and the Effect of N,O-carboxymethyl Chitosan on Postsurgical Healing. Surgery 1997;121:314-9.

[25] Tamer TM, Hassan MA, Valachová K, Omer AM, El-Shafeey ME, Eldin MS, et al. Enhancement of Wound Healing by Chitosan/hyaluronan Polyelectrolyte Membrane Loaded with Glutathione: in Vitro and in Vivo Evaluations. J Biotechnol 2020;310:103-13.

[26] Tamer TM, Valachová K, Hassan MA, Omer AM, El-Shafeey M, Eldin MS, et al. Chitosan/Hyaluronan/Edaravone Membranes for Anti-inflammatory Wound Dressing: In vitro and in vivo Evaluation Studies. Mater Sci Eng C 2018;90:227-35.

[27] Hassan MA, Tamer TM, Valachová K, Omer AM, El-Shafeey M, Eldin MS, et al. Antioxidant and Antibacterial Polyelectrolyte Wound Dressing Based on Chitosan/ Hyaluronan/Phosphatidylcholine Dihydroxycereton. Int J Biol Macromol 2021;166:18-31.

[28] Kimura S, Tsuji T. Mechanical and Immunological Regulation in Wound Healing and Skin Reconstruction. Int J Mol Sci 2021;22:5474.

[29] An Y, Lin S, Tan X, Zhu S, Nie F, Zhen Y, et al. Exosomes from Adipose-derived Stem Cells and Application to Skin Wound Healing. Cell Prolif 2021;54:e12993.

[30] Mazini L, Rochette L, Hamdan Y, Malka G. Skin Immunomodulation during Regeneration: Emerging New Targets. J Pers Med 2021;11:85.
[31] Raziyeva K, Kim Y, Zharkinbekov Z, Kassymbek K, Jimi S, Saparov A. Immunology of Acute and Chronic Wound Healing. Biomolecules 2021;11:700.

[32] Page MJ, McKenzie JE, Bossuyt PM, Boutron I, Hoffmann TC, Mulrow CD, et al. The PRISMA 2020 Statement: An Updated Guideline for Reporting Systematic Reviews. Syst Rev 2021;10:899.

[33] Sterne JA, Hernández MA, Reeves BC, Savović J, Berkman ND, Viswanathan M, et al. ROBINS-I: A Tool for Assessing Risk of Bias in Non-randomised Studies of Interventions. BMJ 2016;355:i4919.

[34] Hilmi AB, Halim AS, Jaafar H, Asiah AB, Hassan A. Chitosan Dermal Substitute and Chitosan Skin Substitute Contribute to Accelerated Full-thickness Wound Healing in Irradiated Rats. Biomed Res Int 2013;2013:795458.

[35] You C, Li Q, Wang X, Wu P, Ho JK, Jin R, et al. Silver Nanoparticle Loaded Collagen/Chitosan Scaffolds Promote Wound Healing Via Regulating Fibroblast Migration and Macrophage Activation. Sci Rep 2017;7:10489.

[36] Rezaei S, Oryan S, Javeri A. Curcumin Nanoparticles Incorporated Collagen-Chitosan Scaffold Promotes Cutaneous Wound Healing Through Regulation of TGF-β1/Smad7 Gene Expression. Mater Sci Eng C Mater Biol Appl 2019;98:347-57.

[37] Zhou M, Lin F, Li W, Shi L, Li Y, Shan G. Development of a Polyamideamine Alginate Composite Dressing for Wound Dressing Application: In vitro and in vivo Evaluations. Int J Pharm 2021;597:120313.

[38] Xiao J, Zhou Y, Ye M, An Y, Wang K, Wu Q, et al. Freeze-Thawing Chitosan/Ions Hydrogel Coated Gauzes Releasing Multiple Metal Ions on Demand for Improved Infected Wound Healing. Adv Healthc Mater 2021;10:e2001591.

[39] Hashemikia S, Farhangpazhouh F, Parsa M, Hasan M, Hassanzadeh A, Hamidi M. Fabrication of Ciprofloxacin-loaded Chitosan/Polyethylene Oxide/Silica Nanofibers for Wound Dressing Application: In vitro and in vivo. Wound Repair Regen 2018;26:497-505.

[40] Lin ZQ, Kondo T, Ishida Y, Takayasu T, Mukaida N. Essential Involvement of IL-6 in the Skin Wound-Healing Process as Evidenced by Delayed Wound Healing in IL-6-Deficient Mice. J Leukoc Biol 2003;73:713-21.

[41] Lin DD, Zimmermann AS, Nauta A, Longaker MT, Lorenz HP. Scarless Fetal Skin Wound Healing Update. Birth Defects Res C Embryo Today 2018;100:999-1015.

[42] Kim T, Zhang Q, Li J, Zhang L, Jokserst JV. A Gold/Silver Hybrid Nanoparticle for Treatment and Photoacoustic Imaging of Bacterial Infection. ACS Nano 2018;12:5615-25.

[43] Shin T, Dai K, Yu Y, Wang J, Liu C. Sulfated Chitosan Rescues Dysfunctional Macrophages and Accelerates Wound Healing in Diabetic Mice. J Biomed Macromol 2021;18:415-24.

[44] Hu B, Gao M, Boakye-Yiadom KO, Ho W, Yu W, Xu X, et al. An Intrinsically Bioactive Hydrogel with on-Demand Drug Release Behaviors for Diabetic Wound Healing. Bioact Mater 2021;6:4592-606.

[45] Li Q, Cui J, Huang H, Yue Z, Chang Y, Li N, et al. IGF-1C Domain-modified Chitosan Hydrogel Accelerates Cutaneous Wound Healing by Promoting Angiogenesis. Future Med Chem 2020;12:1239-51.
Healing and Interventions to Promote Pro-wound Healing Phenotypes. Front Physiol 2018;9:419.

[58] Boniakowski AE, Kimball AS, Jacobs BN, Kunkel SL, Gallagher KA. Macrophage-Mediated Inflammation in Normal and Diabetic Wound Healing. J Immunol 2017;199:17-24.

[59] Aitcheson SM, Frentiu FD, Hurn SE, Edwards K, Murray RZ. Skin Wound Healing: Normal Macrophage Function and Macrophage Dysfunction in Diabetic Wounds. Molecules 2021;26:4917.

[60] Bonito V, Smits AJP, Goor OJG, Ippel BD, Driessen-Mol A, Münker TJA, et al. Modulation of macrophage phenotype and protein secretion via heparin-IL-4 functionalized supramolecular elastomers. Acta Biomater 2018;71:247-60.

[61] Schirmer L, Atallah P, Werner C, Freudenberg U. StarPEG-Heparin Hydrogels to Protect and Sustainably Deliver IL-4. Adv Healthc Mater 2016;5:3157-64.

Publisher’s note

Whioce Publishing remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.