In-silico Feedback Control of a MIMO Synthetic Toggle Switch via Pulse-Width Modulation

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Abstract—The synthetic toggle switch, first proposed by Gardner & Collins\textsuperscript{1} is a MIMO control system that can be controlled by varying the concentrations of two inducer molecules, aTc and IPTG, to achieve a desired level of expression of the two genes it comprises. It has been shown\textsuperscript{2} that this can be accomplished through an open-loop external control strategy where the two inputs are selected as mutually exclusive periodic pulse waves of appropriate amplitude and duty-cycle. In this paper, we use a recently derived average model of the genetic toggle switch subject to these inputs to synthesize new feedback control approaches that adjust the inputs duty-cycle in real-time via two different possible strategies, a model-based hybrid PI-PWM approach and a so-called Zero-Average dynamics (ZAD) controller. The controllers are validated in-silico via both deterministic and stochastic simulations (SSA) illustrating the advantages and limitations of each strategy.

I. INTRODUCTION

The Genetic Toggle Switch is a genetic network of two mutually repressive genes\textsuperscript{1} as shown in Fig. 1. Each promoter activates the translation of a protein that represses the other promoter. External inducers enhance the proteins production by reducing the repressive effect on the promoter made by the opposite protein.

From a dynamical point of view, the toggle switch is a bistable system, with three equilibria, two stable and one unstable. The two stable equilibria correspond to one gene expression being high while the other is low, while at the unstable equilibrium neither of the two proteins is fully expressed. Obviously, in-vivo, this situation cannot be maintained for a long time since biological noise drives the circuit onto one of the two stable equilibria.

The problem of controlling the toggle switch dynamics has been the subject of many papers in the literature, and was recently highlighted in\textsuperscript{2} as the genetic equivalent of controlling an inverted pendulum. For example, Pulse-Shaping Control\textsuperscript{3,4}–\textsuperscript{5} and a Reinforcement Learning control approach\textsuperscript{6} were both proposed to drive the system from a stable equilibrium to the other. Moreover, Stochastic Motion Planning\textsuperscript{7} and Piecewise Linear Switched Control\textsuperscript{8} were used to stabilize the circuit around its unstable equilibrium. In all these cases though the results are only tested in-silico and no experimental validation is provided.

To the best of our knowledge, the only in-vivo control experiment of the toggle switch was reported in\textsuperscript{2}. Therein, the authors propose and validate in-vivo different control strategies to stabilize a population of toggle switches in a region surrounding their unstable equilibrium. Firstly, a PI-based solution is used to close the control loop over a single cell. It is observed that, while the cell being controlled achieves the target region, the others diverge settling down on either of the two stable equilibria. Secondly, it is shown that, despite closing the loop on a single cell, a bang-bang control approach is surprisingly able to stabilize the entire population using pulse wave inputs. Also, inspired by the Kapitza Method for the stabilization of the inverted pendulum\textsuperscript{9}, it is reported that an open-loop periodic forcing of the system via two mutually exclusive pulse waves of appropriate frequency and amplitude achieves stabilization of the entire cell population keeping the variance across the population low. The problem remains of how to select the required features of the inputs and also of guaranteeing greater robustness given that the strategy is open loop. In this paper, we leverage our previous modelling work, reported in\textsuperscript{10}, to synthesize new feedback control strategies able to keep a population of toggle switches at an intermediate level of expression of the genes away from the two stable equilibria. In so doing, we exploit the observation made in\textsuperscript{2} that the use of two mutually exclusive pulse wave inputs can enhance coherence in the population. We show that our approach is effective in solving the control problem offering a viable and relatively simple approach to achieve in-vivo external control of a population of genetic toggle switches.

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Fig. 1. Genetic Toggle Switch as a MIMO System. Inputs are molecules of aTc and IPTG in the growth medium, outputs are fluorescence measures proportional to the concentrations of proteins.
II. THE TOGGLE SWITCH AS A MIMO CONTROL SYSTEM

The deterministic model of the genetic toggle switch that we consider is [2]:

\[
\frac{d mRNA_{LacI}}{dt} = \kappa_{m0} + \frac{\kappa_{m}}{1 + (\frac{T_{tetR}}{\theta_{tetR}} \cdot \frac{1}{g_{T} \cdot (aTc/\eta_{tetR}) / \eta_{tetR}})} \cdot \eta_{tetR} - g_{L} \cdot mRNA_{LacI}
\]

(1)

\[
\frac{d mRNA_{tetR}}{dt} = \kappa_{m0} + \frac{\kappa_{m}}{1 + (\frac{LacI}{\eta_{tetR}} \cdot \frac{1}{\eta_{tetR}} \cdot (IPTG(g_{TPTG} / \eta_{tetR})))) \cdot \eta_{tetR}} - g_{T} \cdot mRNA_{tetR}
\]

(2)

\[
\frac{d LacI}{dt} = \kappa_{p} \cdot mRNA_{LacI} - g_{L} \cdot LacI
\]

(3)

\[
\frac{d TetR}{dt} = \kappa_{p} \cdot mRNA_{tetR} - g_{T} \cdot TetR
\]

(4)

In the above equations, the state variables represent the concentration of mRNAs and proteins of the LacI and TetR promoters. The parameters \( \kappa_{m0}, \kappa_{m}, \kappa_{p}, g_{L}, g_{T} \) are the transcription, translation, mRNA degradation, and protein degradation rates. The inducer molecules \( aTc \) and \( IPTG \) influence the mRNA transcription rates through Hill functions that depend on the regulation parameters \( \theta_{aTc}, \theta_{tetR}, \theta_{LacI}, \theta_{tetR}, \eta_{tetR}, \eta_{tetR}, \eta_{tetR}, \eta_{tetR} \). All parameter values are the same as those used in [2] and are also provided in Table I.

The inducer molecules diffuse across the cell membrane with non-symmetrical dynamics as described in [2]. Specifically, we have

\[
\frac{daTc}{dt} = \begin{cases} 
\kappa_{in}(aTc - aTc), & \text{if } aTc > aTc \\
\kappa_{in}(aTc - aTc), & \text{if } aTc \leq aTc
\end{cases}
\]

(5)

\[
\frac{dIPTG}{dt} = \begin{cases} 
\kappa_{in}(IPTG - IPTG), & \text{if } u_{IPTG} > IPTG \\
\kappa_{in}(IPTG - IPTG), & \text{if } u_{IPTG} \leq IPTG
\end{cases}
\]

(6)

where \( aTc \) and \( IPTG \) denote the concentrations of the inducer molecules inside the cell, while \( u_{aTc} \) and \( u_{IPTG} \) those in the growth medium and represent the inputs to our system. Under certain hypotheses on the ratio between the concentration of the external inducers, the system shows a bistable dynamics [1]. Conversely, when the ratio between the external inducers reaches a certain value, a saddle-node bifurcation occurs and the system becomes monostable.

Since the time scales of the mRNA dynamics is notably faster than that of the proteins, as discussed in [10], by setting \( \frac{d mRNA_{LacI}}{dt} = 0 \) and \( \frac{d mRNA_{tetR}}{dt} = 0 \) we can obtain the nondimensional Quasi-Steady State Model (see [10] for the derivation):

\[
\frac{dx_1}{dt'} = k_1 \cdot \frac{1}{1 + x_2^2} \cdot w_1(t'/g^p) - x_1
\]

\[
\frac{dx_2}{dt'} = k_2 \cdot \frac{1}{1 + x_2^2} \cdot w_2(t'/g^p) - x_2
\]

(7)

where \( t' = g^p \cdot t \), \( x_1 = \frac{LacI}{\theta_{LacI}} \), \( x_2 = \frac{TetR}{\theta_{TetR}} \).

and the adimensional parameters are defined as

\[
k_1 = \frac{\kappa_{L} \cdot m0 \cdot \kappa_{L}}{g_{L} \cdot \theta_{LacI} \cdot g^p}, \quad k_1 = \frac{\kappa_{m} \cdot \kappa_{L}}{g_{L} \cdot \theta_{LacI} \cdot g^p}
\]

(8)

\[
k_2 = \frac{\kappa_{T} \cdot m0 \cdot \kappa_{T}}{g_{T} \cdot \theta_{tetR} \cdot g^p}, \quad k_2 = \frac{\kappa_{m} \cdot \kappa_{T}}{g_{T} \cdot \theta_{tetR} \cdot g^p}
\]

The inputs to the system are modelled by the nonlinear functions \( w_1 \) and \( w_2 \) defined as:

\[
w_1(aTc(t)) = \frac{1}{1 + (\frac{aTc(t)}{\theta_{aTc}}) \cdot \eta_{tetR}} \cdot \eta_{tetR}
\]

\[
w_2(IPTG(t)) = \frac{1}{1 + (\frac{IPTG(t)}{\theta_{IPTG}} \cdot \eta_{tetR})} \cdot \eta_{tetR}
\]

A schematic of the Toggle Switch model [7] represented as a MIMO system is presented in Fig. 1 Therein, the input variables, namely \( aTc \) and \( IPTG \), represent the concentrations of the inducers inside the cell and the output variables \( y_1 \) and \( y_2 \) are fluorescent markers proportional to the concentration of the proteins, RFP for LacI and GFP for TetR, given by

\[
\begin{align*}
y_1 &= k_{RFP} \cdot LacI \\
y_2 &= k_{GFP} \cdot TetR
\end{align*}
\]

TABLE I

| Value of the Parameters of the Model |
|---------------------------------------|
| \( k_{L} \) \( m0 \) | 3.20e-2 | 1.386e-1 |
| \( k_{p} \) | 1.19e-1 | 1.386e-1 |
| \( \theta_{LacI} \) | 8.30 | 1.65e-2 |
| \( \theta_{tetR} \) | 2.06 | 1.65e-2 |
| \( \theta_{LacI} \) | 9.72e-1 | 2.75e-2 |
| \( \theta_{tetR} \) | 1.170 | 1.11e-1 |
| \( \eta_{tetR} \) | 1.62e-1 | 2.00e-2 |
| \( \eta_{tetR} \) | 31.94 | 2.00 |

III. CONTROL DESIGN

In this section we present three control strategies to regulate the expression level of the toggle switch to an arbitrary intermediate value. As input signals we use pulse waves like those recently proposed in [2]. Therein the authors showed both in-silico and in-vivo that such class of input signals has beneficial effects on the level of coherence of the cell population response. This effect has been also recently analyzed in [11].

All stochastic simulations presented in this section were obtained using the Gillespie’s Stochastic Simulation Algorithm (SSA) [12] to accurately take into account the intrinsic biochemical noise of the cells [13].
A. PI control at the population level

As a benchmark, we start by considering a control strategy consisting of two independent PI controllers, one per channel, whose respective loops are closed on the averages of the reporters’ fluorescence over the population rather than on a single cell, as done in [2]. As reported in Fig. 3(a), we observe that, although the mean values of fluorescence are regulated in a neighbourhood of the target point, the population splits in two groups with cells converging onto either of the stable equilibria.

To reduce this high variance across the population, as suggested in [2], we exploit the benefits of using pulse wave inputs by modulating the control inputs generated by the PIs via PWM (Fig. 2). This leads to higher coherence among cells (see Fig. 3(b)) but to higher regulation errors, too.

B. Control via mutually exclusive pulse wave inputs

To overcome the problems of the PI approach presented above, we next modulate in a closed-loop manner two mutually exclusive pulse wave inputs as done in an open-loop experiment reported in [2]. Specifically, we choose

\[ u_{\text{aTc}}(t) = \bar{u}_{\text{aTc}} \cdot s_q(t/T) \]

\[ u_{\text{IPTG}}(t) = \bar{u}_{\text{IPTG}} \cdot (1 - s_q(t/T)) \]

with \( s_q(t/T) \) being a unitary pulse wave signal of period \( T \) and duty-cycle \( D \in [0,1] \), and \( \bar{u}_{\text{aTc}} \) and \( \bar{u}_{\text{IPTG}} \) their amplitudes. The system can then be seen as a SIMO - single input, multiple output - system, as shown in Fig. 4.

During the synthesis, we assume instantaneous diffusion of the inducers across the cell membrane by setting:

\[ aTc(t) = u_{\text{aTc}}(t) \text{ and } IPTG(t) = u_{\text{IPTG}}(t), \forall t \geq t_0. \]

We will then evaluate the effect of diffusion of the inputs across the cell membrane during validation in order to assess robustness of the control strategy.

With these assumptions on the inputs, we previously showed in [10] that, by applying nonlinear averaging techniques, an average model can be obtained that under some conditions captures the mean level of expression of the proteins over each period. Specifically, by rescaling time setting \( \tau = \frac{t}{T} \) and integrating model (7) over a period \( T \), the toggle switch dynamics subject to (9) can be described by the system (see [10] for details)

\[ \frac{dx_1}{dt} = \varepsilon \left[ k_1^0 + k_1 \left( \frac{D}{1 + x_2^2 \cdot \bar{w}_1} + \frac{1 - D}{1 + x_2^2} \right) - x_1 \right] \]

\[ \frac{dx_2}{dt} = \varepsilon \left[ k_2^0 + k_2 \left( \frac{D}{1 + x_1^2 \cdot \bar{w}_2} + \frac{1 - D}{1 + x_1^2} \right) - x_2 \right] \]

(10)

where \( \varepsilon = Ty^p \), \( \bar{w}_1 = w_1(\bar{u}_{\text{aTc}}) \), and \( \bar{w}_2 = w_2(\bar{u}_{\text{IPTG}}) \).

Note that, by varying the amplitudes \( \bar{u}_{\text{aTc}} \) and \( \bar{u}_{\text{IPTG}} \) and the duty-cycle \( D \) of the inputs (9), the unique stable equilibrium point of system (10) changes its location in state space so that different equilibrium curves, say \( \Gamma_i(\bar{u}_{\text{aTc}}, \bar{u}_{\text{IPTG}}) \), parameterized in \( D \) can be obtained by varying the amplitudes of the input signals (see Fig. 5 for some examples of such curves).

We will exploit model (10) to synthesize two alternative feedback control strategies to select the amplitude of the input signals and vary on-line their duty-cycle to stabilize the toggle switch in a region where the genes are expressed at desired intermediate levels.

1) PI-PWM duty cycle compensation: The first approach we propose is a hybrid model-based strategy, whose block diagram is reported in Fig. 6. Here, the average model reported above is used to compute in feedforward the re-
The required amplitudes of the input signals, $\bar{u}_{\text{aTc}}$ and $\bar{u}_{\text{IPTG}}$, and the nominal value of the duty-cycle $D_{\text{ref}}$ required to achieve convergence of the toggle switch in a neighborhood of the desired values of the gene expression encoded by the reference signal.

In absence of disturbances, diffusion dynamics and other unwanted effects, this feedforward action would itself suffice to achieve the control goal. To guarantee robustness when this unavoidable effects are present, a discrete-time feedback PI action is also added to dynamically adjust at the end of each period the duty-cycle to compensate the mismatch between the average cell response predicted by the model and the one being measured. We next describe in greater detail the key components of the control strategy shown in Fig. 6 Model Based Inversion block. This block uses model (10) to select the amplitudes, $\bar{u}_{\text{aTc}}$ and $\bar{u}_{\text{IPTG}}$, and the nominal value of the duty cycle $D_{\text{ref}}$ that yield the equilibrium point closest to the desired reference target point $\bar{x}^\text{ref}_{\text{av}}$. To do so, a database of equilibrium curves such as those depicted in Fig. 5 is interrogated. In our implementation, the database contains a total of 60 equilibrium curves, say $\Gamma_i(\bar{u}_{\text{aTc}}, \bar{u}_{\text{IPTG}})$, $i = 1, \ldots, 60$, parameterized in $D_{\text{ref}}$ that were constructed by using the average model. The curves were obtained by considering values of $\bar{u}_{\text{aTc}} \in [0, 100]$ with a step size of 5 and $\bar{u}_{\text{IPTG}} \in [0, 1]$ with a step size of 0.05. Specifically, 20 curves were obtained by varying $\bar{u}_{\text{IPTG}}$ while keeping constant $\bar{u}_{\text{aTc}} = 100$, 20 curves by varying $\bar{u}_{\text{aTc}}$ with $\bar{u}_{\text{IPTG}} = 1$ and 20 by varying simultaneously $\bar{u}_{\text{aTc}}$ and $\bar{u}_{\text{IPTG}}$ while keeping their ratio constant. Projection block II. Using the values of $\bar{u}_{\text{aTc}}$, $\bar{u}_{\text{IPTG}}$ and $D_{\text{ref}}$ computed in feedforward, the toggle switch evolution under PWM control inputs should converge towards a periodic orbit of period $T$ with average value equal to the equilibrium point selected by the model inversion block. In practice, disturbances, noise and diffusion effects will make this average value different from the predicted one.

At the end of each period, the projection block II computes the error $e_{k,\pi}$ as the length of the arc on the selected equilibrium curve $\Gamma(\bar{u}_{\text{aTc}}, \bar{u}_{\text{IPTG}})$ between the projections onto the same curve of the reference point $\bar{x}^\text{ref}_{\text{av}}$ and the current average state $\langle x(k) \rangle$ (Fig. 7), evaluated as:

\[
\langle x(k) \rangle = \frac{1}{T} \int_{kT}^{(k+1)T} x(\tau) \, d\tau.
\]

PI Controller. Finally, the error $e_{k,\pi}$ is compensated by a PI controller that evaluates the correction $\delta D_k$ to the duty-cycle at each period as:

\[
\delta D_k = k_p \, e_{k,\pi} + k_i \sum_{j=0}^{k} e_{j,\pi},
\]

so that the duty-cycle $D_k$ is then set as $D_k = D_{\text{ref}} + \delta D_k$, starting from $D_0 = D_{\text{ref}}$. A zero-order hold (ZOH) is then used to close the loop via a pulse-width modulator (PWM).

The performance of this controller was validated via both deterministic and stochastic simulations. As shown in Fig. 8(a) when diffusion is present the open loop controller based on the use of solely the model inversion block is unable to guarantee convergence towards the desired values.
Concentrations of the inducer molecules inside and outside the cells, reported as thick line and shaded areas, respectively;

Bottom panels: Duty-Cycle strategies have been numerically tuned to reduce the settling time and the steady state error; their values are

The technique, Zero Average Dynamics control – a PWM-based control strategy originally presented in [14]. The technique has been developed to control electrical converters; however, its adaptability led to its application to several different fields, including Synthetic Biology [15].

Closing the loop instead makes the controller able to drive the toggle switch so that the expression levels of the proteins oscillate around the desired values with the duty-cycle being dynamically adjusted as expected.

Figure 8(c) shows a stochastic simulation for a population of 17 cells. Here the loop is closed onto a single cell (depicted by thicker red and green lines in the figure). We notice that the strategy is able to drive that cell towards the desired steady-state values but also to keep the standard deviation across the population contained in sharp contrast with the average PI controller whose performance has been shown in Fig. 8(a). This is also confirmed by Fig. 8(d) where the evolution of the cell population is averaged over 10 stochastic simulations.

2) ZAD: As an alternative approach, we remove the need for model-based inversion by considering a different strategy, Zero Average Dynamics control – a PWM-based control strategy originally presented in [14]. The technique has been developed to control electrical converters; however, its adaptability led to its application to several different fields, including Synthetic Biology [15].

The control scheme is reported in Fig. 9. The goal of the ZAD controller is to generate at each period T two mutually exclusive pulse waves whose duty-cycle D_k is such that the average value of some function \( \sigma(x(t)) \) is zero, that is

\[
\mathbb{E}_T[\sigma(x(t))] = \int_{kT}^{(k+1)T} \sigma(x(\tau)) d\tau = 0. \tag{11}
\]

By exploiting the fact that at regime there is a one-to-one correspondence of the average values of the state variables...
LacI and TetR (Fig. 5), we choose

$$\sigma(x(t)) = x_1(t) - x_1^{ref} = (LacI(t) - LacI^{ref}) / \theta_{LacI},$$

where the dynamics of $x_1$ is described in (2), under the assumption of instantaneous diffusion. Note that the monotonic dependence of the state variables at steady state with respect to the inputs $u_{aTc}$ and $u_{IP_{TGG}}$ also guarantees attractiveness of the surface defined by $\{\sigma(x) = 0\}$.

By considering a piecewise-linear approximation of $\sigma(t)$ in each period, the duty-cycle is found as:

$$D_k = 1 - \sqrt{\frac{2\sigma_k + T\sigma_{\text{on}}}{T(\sigma_{\text{on}} - \sigma_{\text{off}})}}$$

where $\sigma_k = \sigma(kT)$ and

$$\sigma_{\text{on}} = \frac{\sigma(x(kT))}{u = [u_{aTc}, 0]}, \sigma_{\text{off}} = \frac{\sigma(x(T))}{u = [0, u_{IP_{TGG}}]}.$$

We validated the ZAD controller in both deterministic and stochastic settings by assuming instantaneous diffusion and then tested its robustness in the presence of diffusion of the control inputs through the cell membranes. Fig. 10(a) shows that the strategy is effective when applied to control the deterministic system in the absence of diffusion with the stochastic simulation reported in Fig. 10(b) also confirming low standard deviation across the entire population.

However, when diffusion dynamics is added to the model, the ZAD controller is unable to guarantee a good performance as shown by the deterministic simulation reported in Fig. 10(c). This is due to the fact that our implementation of the ZAD controller does not take diffusion explicitly into account in computing $D_k$. Indeed, the presence of diffusion introduces an undesirable delay in the system which disrupts the ability of the ZAD controller to achieve the control goal and would need to be appropriately compensated. This is the subject of ongoing work which will be reported elsewhere.

IV. Conclusions

We discussed two feedback control strategies to stabilize a genetic toggle switch in a region where the expression levels of the two genes are intermediate. We started from the observation reported in [2] that the use of mutually exclusive pulsing inputs can stabilize the switch in a region surrounding its unstable equilibrium guaranteeing limited standard deviation across the cell population being controlled. To overcome the unavoidable limitations of the open-loop control approach proposed therein, we exploited an average model of the toggle switch subject to this type of inputs to synthesize feedback control approaches able to adjust online the duty-cycle of the periodic inputs. We showed that a model-based PI-PWM strategy for duty-cycle compensation is effective in achieving the desired target region for the expression levels of the genes while also guaranteeing coherence of the fluorescence levels across the cell population. A second strategy based on the ZAD approach was shown to be viable when diffusion is not explicitly taken into account but exhibited limitations otherwise. Future work will be aimed at improving our current ZAD implementation and developing an alternative approach based on MPC to select the duty-cycle of the periodic, mutually exclusive inputs.

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