Compromised Blood–Brain Barrier Integrity Is Associated With Total Magnetic Resonance Imaging Burden of Cerebral Small Vessel Disease

Yue Li1†, Man Li2†, Long Zuo2, Qinglei Shi3, Wei Qin1, Lei Yang1, Tao Jiang2* and Wenli Hu1*

1Department of Neurology, Beijing Chao-Yang Hospital, Capital Medical University, Beijing, China, 2Department of Radiology, Beijing Chao-Yang Hospital, Capital Medical University, Beijing, China, 3Diagnosis Imaging, Siemens Healthcare Ltd., Beijing, China

Objective: Several studies have demonstrated that compromised blood–brain barrier (BBB) integrity may play a pivotal role in the pathogenesis of individual cerebral small vessel disease (cSVD) markers, but the association between BBB permeability and total magnetic resonance imaging (MRI) cSVD burden remains unclear. This study aimed to investigate the relationship between BBB permeability and total MRI cSVD burden.

Methods: Consecutive participants without symptomatic stroke history presented for physical examination were enrolled in this cross-sectional study. The presence of lacunes, white matter hyperintensities (WMH), cerebral microbleeds, and enlarged perivascular spaces was recorded in an ordinal score (range 0–4). We used dynamic contrast-enhanced-MRI and Patlak pharmacokinetic model to quantify BBB permeability in the normal-appearing white matter (NAWM), WMH, cortical gray matter (CGM), and deep gray matter (DGM).

Results: All 99 participants averaged 70.33 years old (49–90 years). Multivariable linear regression analyses adjusted for age, sex, and vascular risk factors showed that leakage rate and area under the leakage curve in the NAWM, WMH, CGM, and DGM were positively associated with total MRI cSVD burden (all P < 0.01). Moreover, fractional blood plasma volumes in the NAWM, CGM, and DGM were negatively associated with total MRI cSVD burden (all P < 0.05).

Conclusion: This study verified that compromised BBB integrity is associated with total MRI cSVD burden, suggesting that BBB dysfunction may be a critical contributor to the pathogenesis of cSVD. Longitudinal studies are required to determine whether there is a causal relationship between BBB permeability and total MRI cSVD burden.

Keywords: cerebral small vessel disease, blood–brain barrier, lacunes, white matter hyperintensities, cerebral microbleeds, enlarged perivascular spaces, dynamic contrast-enhanced-magnetic resonance imaging
INTRODUCTION
Cerebral small vessel disease (cSVD) is a general term commonly used to describe a group of pathological processes involving perforating cerebral arterioles, capillaries, and venules (1). Lacunes, white matter hyperintensities (WMH), cerebral microbleeds (CMBs), and enlarged perivascular spaces (EPVS) have been identified as magnetic resonance imaging (MRI) markers of cSVD (2). CSVD is associated with an increased risk of stroke, cognitive impairment, and gait abnormalities (3). The pathogenesis of cSVD has not been completely understood but evidence is mounting that blood–brain barrier (BBB) dysfunction is a contributing factor (4).

Dynamic contrast-enhanced (DCE)-MRI combined with an appropriate pharmacokinetics model is a reliable method to quantitatively evaluate BBB permeability (5). Using DCE-MRI method, previous cross-sectional studies reported compromised BBB integrity in patients with lacunar stroke, WMH, and mild vascular cognitive impairment (nVCI) (6–10). Moreover, a longitudinal study (11) revealed the association between poor functional outcome and increased BBB permeability in cSVD patients. However, these studies mostly focused on single MRI markers of cSVD, and no studies have investigated the combined effects of cSVD features to date.

Recently, Staals et al. (12) proposed a validated scale to evaluate comprehensive cSVD burden (range 0–4) by summing different MRI features, including lacunes, WMH, CMBs, and EPVS. Since the four cSVD markers are often correlated instead of occurring separately, this total MRI cSVD burden may be a more appropriate method to represent their combined effects.

A previous study (8) has chosen the normal-appearing white matter (NAWM), WMH, cortical gray matter (CGM), and deep gray matter (DGM) as regions of interest (ROIs) and demonstrated a larger tissue volume with subtle BBB leakage in cSVD patients than in the controls, thus supporting the generalized nature of cSVD. This study aimed to verify whether BBB permeability increased with the aggravation of total MRI cSVD burden in these ROIs. To exclude the effect of symptomatic stroke on BBB permeability (13), participants with symptomatic stroke history were not selected for this study. In addition, we tentatively examined whether each of the MRI markers was independently associated with BBB permeability change.

MATERIALS AND METHODS
Study Population
We recruited consecutive participants presented for physical examination at the department of Neurology in Beijing Chao-Yang Hospital, Capital Medical University, from May 2016 to April 2017. Exclusion criteria included: (1) history of symptomatic stroke or carotid stenosis of ≥50%, epilepsy, Alzheimer disease, neurodegenerative disease, and other neurological disorders; (2) tumor, brain trauma, systemic inflammatory disease; (3) contraindication for MRI (e.g., metal implants, pacemaker, and claustrophobia) or the use of the contrast agent (e.g., renal failure or allergy to gadolinium); and (4) alcohol or drug abuse, psychiatric disorders (e.g., depression or schizophrenia).

Ethics Statement
All participants consented to participate in our study and signed an informed consent to the use of data for research. The design of this study was approved by the Ethics Committee of Beijing Chao-Yang Hospital, Capital Medical University and was performed in accordance with the declaration of Helsinki.

MRI Protocol and Assessment
Structural MRI
All participants underwent structural brain MRI on a 3T MRI scanner (Prisma; Siemens AG, Erlangen, Germany). Sequences included diffusion-weighted imaging, T1-weighted (T1-W), T2-weighted (T2-W), fluid-attenuated inversion recovery (FLAIR), and susceptibility-weighted imaging (SWI), respectively. MRI sequence parameters are provided in Table S1 in Supplementary Material.

Dynamic Contrast-Enhanced (DCE)-MRI
Magnetic resonance imaging examinations were performed on a 3T MRI scanner (Prisma; Siemens AG, Erlangen, Germany). T1 dynamic protocol comprises precontrast T1 measurements with two different flip angles (3°, 15°) for T1 mapping, as well as continuous serial acquisitions of 60 volumes of T1-W images. The sequence was applied [repetition time (TR)/echo time (TE) 5.08/1.8 ms, field of view 230 mm × 230 mm, voxel size 1.2 mm × 1.2 mm × 3 mm]. After start of acquisition of four volumes of T1-W images, the contrast agent (gadolinium, 1.0 mmol/mL; 0.1 mmol/kg body weight, range 5–10 mmol per person) was administered in the antecubital vein at a rate of 2.5 mL/s using a power injector, followed by a 20 mL saline flush.

MR Imaging Analysis
DCE-MRI data were processed offline using Nordic ICE (Nordic Neuro Lab, Bergen, Norway). The concentration of contrast agent in tissue was calculated using relative signal change and T1 mapping. Individual vascular input functions were derived from the superior sagittal sinus (14) using a semi-automated method in the Nordic ICE (Nordic Neuro Lab) software. The Patlak graphical approach that was identified as the most appropriate model for low-leakage regimen was applied per voxel (15). The Patlak graphical approach provided BBB leakage rate ($K_{trans}$), area under the leakage curve (AUC), and fractional blood plasma volume ($V_p$).

Regions of Interest
We used an axial T2 FLAIR MRI sequence with the same orientation and slice thickness as our DCE sequence to manually draw ROIs in the NAWM, WMH, CGM, and DGM in both hemispheres (Figure 1) (16). CGM was placed at prefrontal cortex (size = 5 mm$^2$) and DGM was placed at lentiform nucleus (size = 5 mm$^2$). Since WMH were divided into periventricular WMH (PVWMH) and deep WMH (DWWMH), we drew ROIs in both areas that were hyperintensive (size = 5 mm$^2$). NAWM (size = 5 mm$^2$) was placed around the WMH lesions. For participants without visible WMH, we strived to match the anatomical location and size of the ROIs as close as possible. The WMH was placed around the periventricular, and NAWM was located in the 10 mm area around the
WMH area. Each ROI was measured for four times and averaged to obtain the average BBB leakage parameters. An experienced radiologist performed this procedure manually.

Assessment of Total MRI cSVD Burden

Neuroimaging markers of cSVD were defined according to Standards for Reporting Vascular Changes on Neuroimaging (STRIVE) criteria (2). Lacunes were defined as round or ovoid fluid-filled cavities of 3–15 mm on T2-W and FLAIR (2). DWMH and PVWMH were graded using the Fazekas scale (17). CMBs were defined as round or ovoid lesions of ≤10 mm with low signal intensity on SWI and categorized according to Microbleed Anatomical Rating Scale (18). EPVS were identified as punctate or linear hyperintensities on T2-W images in the basal ganglia (BG) or centrum semiovale. A 4-point visual rating ordinal scale (0, no EPVS; 1, 1–10 EPVS; 2, 11–20 EPVS; 3, 21–40 EPVS; 4, >40 EPVS) was used to evaluate the severity of EPVS (19).

We used the recently reported scale to represent the total MRI cSVD burden by counting the presence of each of the four features of cSVD (12). A point was awarded for each of the following items: ≥1 lacune; Fazekas score ≥2 in deep white matter (DWM) and/or Fazekas score of 3 in periventricular white matter (PVWM); ≥1 deep or infratentorial CMBs (20); moderate to extensive (grade 2–4) EPVS in the BG (19). Hence, the score ranged from 0 to 4 points.

All images were analyzed by two experienced radiologists blinded to the clinical data. An interobserver reliability test was performed in 35 subjects, and the κ-coefficient for lacunes, WMH, CMBs, and EPVS was 0.815, 0.792, 0.832, and 0.791, respectively. Disagreement was resolved by discussing with other coauthors.

Statistical Analysis

Continuous variables with normal distribution were presented as mean with SD and compared using one-way analysis of variance, followed by Student–Newman–Kuels multiple comparison test. Variables with non-normal distribution were presented as median with interquartile ranges and compared using Kruskal–Wallis test. Bonferroni correction was used for post hoc comparisons. Categorical variables were compared using chi-square tests. The associations between BBB permeability parameters and total MRI cSVD burden were examined using Spearman correlation analysis. Subsequently, the association between BBB permeability with total MRI cSVD burden was investigated using univariable linear regression analyses. Multivariable linear regression analyses were then used to adjust for age, sex, and vascular risk factors.

Coefficients of determination (R²) were calculated in univariable linear regression analyses to determine the proportion of variance in BBB permeability explained by total MRI cSVD burden. To investigate the contribution of each of the MRI markers, we repeated the analysis with lacunes, WMH, CMBs, and EPVS as independent variables individually (dichotomized, as defined above) and R² were calculated. In addition, R² of Fazekas score (range 0–6) were calculated. Statistical significance was established at P < 0.05. Analysis was performed with Statistical Package for Social Sciences (version 24).

RESULTS

Participants Characteristics

A total of 139 participants were recruited but 40 were excluded (12 participants with incomplete injection of contrast or contraindications for MRI, 18 participants with history of symptomatic stroke or carotid stenosis, and the other 10 participants with history of tumor). In the end, 99 participants (70.33 ± 9.07 years; 49.5% male) were enrolled.

For total MRI cSVD burden, 31 (31.31%) participants had a total cSVD score of 0; 25 (25.25%), 1; 16 (16.16%), 2; 15 (15.15%), 3; and 12 (12.12%), 4, respectively. The prevalence of each cSVD marker was lacunes, 38 (38.38%); WMH, 47 (47.47%); CMBs, 24 (24.24%); and EPVS, 41 (41.41%), respectively. Clinical characteristics of participants are presented in Table 1. There was no significant difference in baseline characteristics and laboratory tests (Table S2 in Supplementary Material) among five groups.

Association Between BBB Permeability and Total MRI cSVD Burden

An example of leakage rate, area under the leakage curve, and fractional blood plasma volume map is displayed in Figure 2. An overview of the quantitative results and statistical results is shown in Table 2. Spearman correlation analysis revealed that in all ROIs, BBB leakage rate, and area under the leakage curve were both positively correlated with total MRI cSVD burden, while
blood plasma volume in the NAWM, CGM, and DGM showed negative correlation with total MRI cSVD burden.

Univariable linear regression analysis revealed that leakage rate and area under the leakage curve in all ROIs were positively associated with total MRI cSVD burden while fractional blood plasma volume in the NAWM, CGM, and DGM was negatively associated with total MRI cSVD burden. These associations remained significant after adjustment for age, sex, and vascular risk factors. These statistical results are displayed in Table 3.

In our research, there are five participants who did not have visible WMH, their WMH ROI was placed around the periventricular, which may cause an ambiguity. Thus, we tentatively took out these five participants and repeated the statistical analysis. Leakage rate and area under the leakage curve in the NAWM, WMH, CGM, and DGM were still positively correlated with total MRI cSVD burden, and the association between higher total MRI cSVD burden and lower fractional blood plasma volume in the NAWM, CGM, and DGM still held. These statistical results are displayed in Tables S3–S5 in Supplementary Material.

Correlations of Determination of Individual MRI Markers

$R^2$, which indicated the proportion of variance in BBB permeability explained by total MRI cSVD burden and each of individual MRI markers, are displayed in Table 4. The magnitude of the individual MRI markers differed across parameters. The dichotomized WMH explained a higher proportion of variance in leakage rate and area under the leakage curve than the presence of lacunes and CMBs in most of ROIs. The proportions of variance in BBB leakage explained by Fazekas score were comparable to those explained by total MRI cSVD burden. Fazekas score explained a higher proportion of variance in fractional blood plasma volume in NAWM, WMH, and CGM than total MRI cSVD burden.

Since the results showed that Fazekas score explained similar or even higher proportions of variance in BBB permeability than the total score, we tentatively examined whether the association still existed if WMH was taken out from the total score. Thus, we designed a new “total score” scale in which WMH was taken out and repeated the statistical analysis. Leakage rate and area under the leakage curve in the NAWM, WMH, CGM, and DGM were still positively correlated with total MRI cSVD burden; and the relationship between higher total MRI cSVD burden and lower fractional blood plasma volume in the NAWM, CGM, and DGM still held. We also calculated the $R^2$ of this new “total score”. These statistical results are displayed in Tables S6 and S7 in Supplementary Material. These results showed that other features of cSVD except for WMH also associated with BBB permeability.

**FIGURE 2** An example map. (A) Axial fluid-attenuated inversion recovery image of a 77-year-old woman; (B) blood-brain barrier leakage rate ($K_{low}$) map; (C) area under the leakage curve map; (D) fractional blood plasma volume ($V_d$) map.

**TABLE 1** Demographic and clinical features of participants with different severity of total MRI cSVD burden.

|                          | Total (n = 99) | cSVD 0 (n = 31) | cSVD 1 (n = 25) | cSVD 2 (n = 16) | cSVD 3 (n = 15) | cSVD 4 (n = 12) | P       |
|--------------------------|---------------|-----------------|-----------------|-----------------|-----------------|-----------------|---------|
| Male, n (%)              | 49 (49.5)     | 13 (41.9)       | 15 (60.0)       | 5 (31.3)        | 8 (53.3)        | 8 (66.7)        | 0.244   |
| Age, years               | 70.33 ± 9.07  | 67.42 ± 9.04    | 70.44 ± 7.88    | 71.06 ± 7.86    | 75.47 ± 10.22   | 70.25 ± 9.87    | 0.722   |
| Hypertension, n (%)      | 65 (65.7)     | 16 (51.6)       | 17 (68.0)       | 11 (68.8)       | 13 (86.7)       | 8 (66.7)        | 0.188   |
| Diabetes mellitus, n (%) | 19 (19.2)     | 5 (16.1)        | 2 (8.0)         | 4 (25.0)        | 3 (20.0)        | 5 (41.7)        | 0.186   |
| Hyperlipidemia, n (%)    | 53 (52.5)     | 14 (45.2)       | 14 (56.0)       | 9 (56.3)        | 9 (60.0)        | 6 (50.0)        | 0.870   |
| Current smoking, n (%)   | 27 (27.3)     | 6 (19.4)        | 9 (36.0)        | 5 (31.3)        | 3 (20.0)        | 4 (33.3)        | 0.605   |
| BMI, kg/m²               | 25.79 ± 3.14  | 25.51 ± 2.49    | 26.37 ± 4.17    | 26.07 ± 2.66    | 25.37 ± 3.40    | 25.44 ± 2.66    | 0.243   |

Data are presented as mean ± SD, median (interquartile range), or counts (%). MRI, magnetic resonance imaging; cSVD, cerebral small vessel disease; n, number of persons; BMI, body mass index.

**DISCUSSION**

The main finding of this study was that BBB permeability in the NAWM, WMH, CGM, and DGM measured by DCE-MRI was positively correlated with total MRI cSVD burden. We also found an association between higher total MRI cSVD burden and lower fractional blood plasma volume in the NAWM, CGM, and DGM.

Previous studies paid much attention to the individual MRI features of cSVD and described associations between compromised BBB integrity and lacunar stroke or WMH (6, 8). We think it is necessary to evaluate the association between total MRI cSVD burden and BBB permeability since total MRI cSVD burden could represent the underlying severity of cSVD better than single MRI markers. Our study comprehensively clarified the association of BBB permeability and cerebral blood flow (CBF) with total MRI cSVD burden.
been frequently reported. Using diffusion tensor imaging and DCE-MRI in combination, Munoz Maniega et al. (9) found that BBB permeability increased with the rise of WMH burden, but they only described BBB leakage rate of WMH and NAWM, and did not evaluate those in the cortex. Zhang et al. (8) found the leakage volume of the NAWM, WMH, and CGM in cSVD and mVCI patients was higher compared with controls, but there was no significant difference in leakage rate in all ROIs. The discrepancy between this study and our study might be explained by differences in the study participants. We excluded participants with a history of symptomatic stroke since stroke may also cause BBB permeability change (13).

The precise mechanism for the relationship between BBB permeability and cSVD is not well established. An experiment was carried out with spontaneously hypertensive stroke-prone rats (SHRSP), and it was conjectured that BBB breakdown may be the starting point of cSVD (21). The change of BBB permeability might mediate a series of pathophysiological changes and eventually lead to cSVD. BBB is a selective barrier structure consists of capillary endothelial cells, pericytes, astrocytes and extracellular matrix (22). Tight junctions (TJs) are an important component of BBB which couple endothelial cells mechanically and prevent toxic substances from leaking into the brain interstitium (23). The breakdown of TJs will result in leakage of plasma content, toxic substances from leaking into the brain interstitium (23). These series of events could explain the pathological and imaging features of lacunar infarctions, WMH, CMs, and EPVs (4). There is a new insight that barrier changes in cSVD is

| TABLE 2 | Leakage rate, area under the leakage curve, and fractional blood plasma volume of participants with different severity of total MRI cSVD burden. |

|          | cSVD 0 (n = 31) | cSVD 1 (n = 25) | cSVD 2 (n = 16) | cSVD 3 (n = 15) | cSVD 4 (n = 12) | P      |
|----------|-----------------|-----------------|-----------------|-----------------|-----------------|--------|
| NAWM     |                 |                 |                 |                 |                 |        |
| Ktrans   | 0.14 (0.05, 0.32) | 0.18 (0.11, 0.36) | 0.30 (0.22, 0.43) | 0.37 (0.22, 0.48) | 0.47 (0.35, 0.55) | <0.001 |
| AUC      | 3.31 ± 1.14    | 3.57 ± 0.99     | 4.75 ± 0.64     | 4.45 ± 1.43     | 4.93 ± 1.43     | <0.001 |
| Vp       | 6.85 ± 2.64    | 5.99 ± 2.45     | 4.76 ± 2.21     | 4.73 ± 2.00     | 5.29 ± 1.90     | 0.015  |
| WMH      |                 |                 |                 |                 |                 |        |
| Ktrans   | 0.28 (0.11, 0.43) | 0.36 (0.19, 0.54) | 0.57 (0.33, 0.94) | 0.56 (0.39, 0.87) | 0.67 (0.55, 0.93) | <0.001 |
| AUC      | 4.00 ± 1.34    | 4.41 ± 1.31     | 6.20 ± 1.89     | 6.50 ± 1.79     | 7.05 ± 1.82     | <0.001 |
| Vp       | 9.49 ± 5.04    | 8.70 ± 4.70     | 9.37 ± 5.15     | 8.43 ± 5.28     | 6.62 ± 3.10     | 0.497  |
| CGM      |                 |                 |                 |                 |                 |        |
| Ktrans   | 0.93 (0.70, 1.26) | 0.97 (0.77, 1.29) | 1.36 (0.99, 2.39) | 1.91 (1.12, 2.44) | 1.59 (1.21, 2.03) | <0.001 |
| AUC      | 14.85 ± 5.96   | 15.64 ± 4.89    | 19.22 ± 4.81    | 18.55 ± 4.98    | 20.02 ± 5.29    | 0.008  |
| Vp       | 27.68 ± 9.91   | 24.65 ± 9.25    | 23.42 ± 9.84    | 22.20 ± 10.05   | 17.91 ± 7.04    | 0.043  |
| DGM      |                 |                 |                 |                 |                 |        |
| Ktrans   | 0.51 (0.30, 0.74) | 0.61 (0.44, 0.90) | 0.72 (0.58, 1.05) | 0.96 (0.67, 1.53) | 1.00 (0.91, 1.47) | <0.001 |
| AUC      | 9.54 ± 3.24    | 10.51 ± 2.26    | 11.92 ± 2.15    | 11.17 ± 2.88    | 12.37 ± 2.60    | 0.009  |
| Vp       | 18.37 ± 6.41   | 18.30 ± 8.06    | 14.75 ± 5.86    | 14.14 ± 6.19    | 11.56 ± 5.44    | 0.011  |

TABLE 3 | Association of leakage rate, area under the leakage curve, and fractional blood plasma volume with total MRI cSVD burden.

|          | Spearman correlation | Univariablea | Multivariablea |
|----------|---------------------|--------------|----------------|
|          | r       | P value | β        | P value | β        | P value |
| NAWM     |         |        |          |         |          |         |
| Ktrans   | 0.558   | <0.001 | 0.082   | <0.001 | 0.082   | <0.001 |
| AUC      | 0.444   | <0.001 | 0.432   | <0.001 | 0.432   | <0.001 |
| Vp       | -0.273  | 0.006  | -0.523  | 0.003  | -0.523  | 0.003  |
| WMH      |         |        |          |         |          |         |
| Ktrans   | 0.573   | <0.001 | 0.149   | <0.001 | 0.154   | <0.001 |
| AUC      | 0.583   | <0.001 | 0.839   | <0.001 | 0.867   | <0.001 |
| Vp       | -0.135  | 0.183  | -0.528  | 0.348  | -0.133  | 0.184  |
| CGM      |         |        |          |         |          |         |
| Ktrans   | 0.500   | <0.001 | 0.245   | <0.001 | 0.230   | <0.001 |
| AUC      | 0.378   | <0.001 | 1.379   | 0.001  | 1.608   | <0.001 |
| Vp       | -0.282  | 0.005  | -2.155  | 0.002  | -2.082  | 0.033  |
| DGM      |         |        |          |         |          |         |
| Ktrans   | 0.489   | <0.001 | 0.173   | <0.001 | 0.173   | <0.001 |
| AUC      | 0.351   | <0.001 | 0.672   | 0.001  | 0.602   | 0.003  |
| Vp       | -0.323  | 0.001  | -1.720  | 0.001  | -1.623  | 0.001  |

MRI, magnetic resonance imaging; cSVD, cerebral small vessel disease; NAWM, normal-appearing white matter; WMH, white matter hyperintensities; CGM, cortex gray matter; DGM, deep gray matter; Ktrans, leakage rate; AUC, area under the leakage curve; Vp, fractional blood plasma volume.

a Significant difference between cSVD 0 and cSVD 2 categories.
b Significant difference between cSVD 0 and cSVD 3 categories.
c Significant difference between cSVD 0 and cSVD 4 categories.
d Significant difference between cSVD 1 and cSVD 2 categories.
e Significant difference between cSVD 1 and cSVD 3 categories.
f Significant difference between cSVD 1 and cSVD 4 categories.

Although lacunes and WMH are often found together, the independent relationship between WMH and BBB leakage has been frequently reported. Using diffusion tensor imaging and DCE-MRI in combination, Munoz Maniega et al. (9) found that BBB permeability increased with the rise of WMH burden, but they only described BBB leakage rate of WMH and NAWM, and did not evaluate those in the cortex. Zhang et al. (8) found the leakage volume of the NAWM, WMH, and CGM in cSVD and mVCI patients was higher compared with controls, but there was no significant difference in leakage rate in all ROIs. The discrepancy between this study and our study might be explained by differences in the study participants. We excluded participants with a history of symptomatic stroke since stroke may also cause BBB permeability change (13).
at the capillary level, which is typically characterized by massive losses of smooth muscle cells and some arterioles could contribute to the loss of cerebrovascular barrier protection (26).

Notably, the association between CMRs and BBB permeability indicated that BBB dysfunction may be a contributor to the pathogenesis of CMRs. A previous study (27) showed that CMRs were linked to the deposition of β-amyloid in small vessel walls while another study (28) revealed that iron deposition might be an indicator of cSVD that predisposes to WMH. These depositions may be attributed to the altered transport systems and deteriorated environment of the neural cells caused by compromised BBB integrity (22).

A number of cSVD MRI markers might be more important than others in the association with BBB permeability. Our results showed that Fazekas score explained similar or even higher proportions of variance in BBB permeability while dichotomized WMH explained smaller proportions of variance, probably because a wider range of severity was captured by the Fazekas score (ranging 0–6) compared with the cSVD score (ranging 0–4). However, we advocate cSVD score as an alternative to Fazekas score (ranging 0–6) compared with the cSVD score (ranging 0–4).

Apart from BBB permeability change, we also found that participants with higher total MRI cSVD burden had a lower fractional blood plasma volume in the NAWM, CGM, and DGM. As blood plasma volume is related to the CBF, this finding is in line with a previous study (29), further illustrating the association between the cSVD and reduced CBF. A meta-analysis of 4 longitudinal and 34 cross-sectional CBF studies also showed that CBF was lower in subjects with more WMH, and most CBF data were from gray matter, which was consistent with our study (30). These results further confirmed the hypothesis that cSVD and CBF are associated with chronic hypoperfusion or impaired cerebrovascular reactivity (1). However, there was no association between higher total MRI cSVD burden and lower fractional blood plasma volume in the WMH in our study. There are three possible reasons. First, in the meta-analysis mentioned earlier, most included studies recorded CBF in CGM, data for white matter were limited, thus, this research emphasized that more CBF data are needed for white matter, especially separate data for NAWM and WMH. Second, some longitudinal studies revealed that decreased CBF was related to progression of PWVMH rather than to that of DWMH. But they also found no association between CBF and volume of total WMH, PVWMH, or DWMH at baseline. The contradictory follow-up result indicated that the vulnerability for DWMH and PVWMH might be different since these two brain areas are on different sections of the arteriolar tree. PWVMH are often located symmetrically in both cerebral hemispheres, that is suggestive of diffuse perfusion disturbance but DWMH frequently have an asymmetrical distribution that is suggestive of local perfusion disturbances. Therefore, it is still unclear whether reduced CBF is the etiology of WMH or secondary reaction of decreased metabolism of injured WM areas. Third, another longitudinal study (31) showed that decreasing CBF was related to progression of PWVMH rather than to that of DWMH. But they also found no association between CBF and volume of total WMH, PVWMH, or DWMH at baseline. The contradictory follow-up result indicated that the vulnerability for DWMH and PWVMH might be different since these two brain areas are on different sections of the arteriolar tree. PWVMH are often located symmetrically in both cerebral hemispheres, that is suggestive of diffuse perfusion disturbance but DWMH frequently have an asymmetrical distribution that is suggestive of local perfusion disturbances. But in our study, we focused on the BBB permeability of overall white matter of the brain, and each ROI was measured for four times and averaged to obtain average parameters. Therefore, we did not divide the white matter into PVWM and DWM. Further studies are required to investigate how hypoperfusion varies across different tissues by using area stratification analysis, and how it changes across the course of the cSVD.

Our study has the following strengths: (1) we used total MRI cSVD burden to analyze the association between cSVD and BBB permeability, which was a more representative and

| Table 4 | For the association between BBB permeability and total MRI cSVD burden versus individual MRI markers. |
|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|
| Total MRI cSVD burden | Lacunes | WMH | Fazekas score | CMBs | EPVS |
|-----------------|-----------------|-----------------|-----------------|-----------------|-----------------|
| NAWM | | | | | |
| $K_{\text{trans}}$ | 0.220 | <0.001 | 0.150 | <0.001 | 0.127 | <0.001 | 0.161 | <0.001 | 0.106 | 0.001 | 0.082 | 0.004 |
| AUC | 0.170 | <0.001 | 0.054 | 0.021 | 0.194 | <0.001 | 0.263 | <0.001 | 0.133 | <0.001 | 0.049 | 0.028 |
| $V_p$ | 0.087 | 0.003 | 0.058 | 0.017 | 0.054 | 0.021 | 0.170 | <0.001 | 0.008 | 0.392 | 0.077 | 0.005 |
| WMH | | | | | |
| $K_{\text{trans}}$ | 0.265 | <0.001 | 0.079 | 0.005 | 0.164 | <0.001 | 0.243 | <0.001 | 0.113 | 0.001 | 0.214 | <0.001 |
| AUC | 0.357 | <0.001 | 0.114 | 0.001 | 0.353 | <0.001 | 0.364 | <0.001 | 0.207 | <0.001 | 0.118 | 0.001 |
| $V_p$ | 0.023 | 0.132 | 0.042 | 0.041 | 0.003 | 0.601 | 0.048 | 0.030 | 0.005 | 0.479 | 0.12 | 0.288 |
| CGM | | | | | |
| $K_{\text{trans}}$ | 0.181 | <0.001 | 0.141 | <0.001 | 0.108 | 0.001 | 0.167 | <0.001 | 0.036 | 0.060 | 0.105 | 0.001 |
| AUC | 0.117 | 0.001 | 0.018 | 0.190 | 0.123 | <0.001 | 0.086 | 0.003 | 0.054 | 0.020 | 0.067 | 0.010 |
| $V_p$ | 0.094 | 0.002 | 0.092 | 0.002 | 0.039 | 0.051 | 0.124 | <0.001 | 0.037 | 0.056 | 0.037 | 0.058 |
| DGM | | | | | |
| $K_{\text{trans}}$ | 0.233 | <0.001 | 0.128 | <0.001 | 0.146 | <0.001 | 0.216 | <0.001 | 0.115 | 0.001 | 0.101 | 0.001 |
| AUC | 0.110 | 0.001 | 0.075 | 0.006 | 0.094 | 0.002 | 0.100 | 0.001 | 0.034 | 0.066 | 0.035 | 0.064 |
| $V_p$ | 0.117 | 0.001 | 0.084 | 0.004 | 0.034 | 0.069 | 0.106 | 0.001 | 0.011 | 0.291 | 0.039 | 0.051 |

$R^2$, coefficient of determination; cSVD, cerebral small vessel disease; WMH, white matter hyperintensities; CMRs, cerebral microbleeds; EPVs, enlarged perivascular spaces; NAWM, normal-appearing white matter; CGM, cortex gray matter; DGM, deep gray matter; $K_{\text{trans}}$, leakage rate; AUC, area under the leakage curve; $V_p$, fractional blood plasma volume; MRI, magnetic resonance imaging; BBB, blood–brain barrier.
comprehensive method to reflect the severity of cSVD; (2) we applied strict exclusion criteria to avoid the effect of BBB permeability change caused by symptomatic stroke; and (3) the Patlak pharmacokinetics we applied is the most suited method to distinguish cSVD-related from age-related BBB permeability change so far (8).

Our study is also subjected to a number of limitations: (1) all MRI markers are dichotomized in the scale, locations and numbers of lacunes, and CMBs are not accounted for in this score; total quantitative load of WMH and EPVS, greater granularity for lacunes as well as CMBs and different weightings and cut points for different cSVD features should be tested in future studies; (2) since we selected participants who received physical examination from a single center, the generalizability of our results to community population may be limited; (3) our study is incapable of investigating whether the change of BBB permeability could predict cSVD progression; longitudinal studies with community-based series of participants are needed to determine whether BBB precedes or follows the various features of cSVD; and (4) in our research, there are five participants who did not have visible WMH, their WMH ROI was placed around the periventricular, which may cause an ambiguity. But in our study, we focused on the relationship between BBB permeability and total MRI cSVD burden, participants without visible WMH may have other cSVD markers, we worried that there would be selection bias if we removed these people. And participants without visible WMH were also not taken out in other similar researches (8, 9, 32). Thus, to avoid selection bias and improve the comparability with similar studies, participants without visible WMH were not excluded from this study.

CONCLUSION
This study indicated that a higher total MRI cSVD burden was associated with larger BBB permeability in the NAWM, WMH, CGM, and DGM, which provides additional evidence that compromised BBB integrity may play a role in the pathogenesis of cSVD. We also observed that participants with a higher total MRI cSVD burden had a lower fractional blood plasma volume in the NAWM, CGM, and DGM. Longitudinal studies are required to confirm a causal relationship between the BBB permeability and cSVD progression.

ETHICS STATEMENT
All participants consented to participate in our study and signed an informed consent to the use of data for research. The design of this study was approved by the Ethics Committee of Beijing Chao-Yang Hospital, Capital Medical University and was performed in accordance with the declaration of Helsinki. The details of each participant are displayed in Tables S8 in Supplementary Material.

AUTHOR CONTRIBUTIONS
Conception and design of the research: TJ and WH. Acquisition of the data: YL, ML, and QS. Analysis and interpretation of the data: YL, ML, and QS. Drafting the manuscript: YL and ML. Critical revision of the manuscript: LZ, WQ, LY, TJ, and WH. Final approval of the version to be published: YL, ML, LZ, QS, WQ, LY, TJ, and WH.

FUNDING
This study was supported by National Natural Science Foundation of China (Grant No. 81271309). The funders had no role concerning study design, data collection and analysis, decision to publish, or preparation of the manuscript.

SUPPLEMENTARY MATERIAL
The Supplementary Material for this article can be found online at https://www.frontiersin.org/articles/10.3389/fneur.2018.00221/full#supplementary-material.

REFERENCES
1. Pantoni L. Cerebral small vessel disease: from pathogenesis and clinical characteristics to therapeutic challenges. *Lancet Neurol* (2010) 9(7):689–701. doi:10.1016/S1474-4422(10)70104-6
2. Wardlaw JM, Smith EE, Biessels GJ, Cordonnier C, Fazekas F, Frayne R, et al. Neuroimaging standards for research into small vessel disease and its contribution to ageing and neurodegeneration. *Lancet Neurol* (2013) 12(8):822–38. doi:10.1016/S1474-4422(13)70124-8
3. Smith EE, Saponnik G, Biessels GJ, Doubl FN, Fornage M, Gorelick PB, et al. Prevention of stroke in patients with silent cerebrovascular disease: a scientific statement for healthcare professionals from the American Heart Association/ American Stroke Association. *Stroke* (2017) 48(2):e44–71. doi:10.1161/STR.0000000000000116
4. Wardlaw JM. Blood-brain barrier and cerebral small vessel disease. *J Neurol Sci* (2010) 299(1–2):66–71. doi:10.1016/j.jns.2010.08.042
5. Heye AK, Thrrippleton MJ, Armitage PA, Valdes Hernandez MDel C, Makin SD, Glatz A, et al. Tracer kinetic modelling for DCE-MRI quantification of subtle blood-brain barrier permeability. *Neuroimage* (2016) 125:446–55. doi:10.1016/j.neuroimage.2015.10.018
6. Topakian R, Barrick TR, Howe FA, Markus HS. Blood-brain barrier permeability is increased in normal-appearing white matter in patients with lacunar stroke and leucoaraisis. *J Neurol Neurosurg Psychiatry* (2010) 81(2):192–7. doi:10.1136/jnnp.2009.172072
7. Taheri S, Gasparovic C, Huisa BN, Adair JC, Edmonds E, Prestopnik J, et al. Blood-brain barrier permeability abnormalities in vascular cognitive impairment. *Stroke* (2011) 42(8):2158–63. doi:10.1161/STROKEAHA.110.611731
8. Zhang CE, Wong SM, van de Haar HJ, Staals J, Jansen JF, Jeukens CR, et al. Blood-brain barrier leakage is more widespread in patients with cerebral small vessel disease. *Neurology* (2017) 88(5):426–32. doi:10.1212/WNL.000000000003556
9. Munoz Maniega S, Chappell FM, Valdes Hernandez MC, Armitage PA, Makin SD, Heye AK, et al. Integrity of normal-appearing white matter: influence of age, visible lesion burden and hypertension in patients with small-vessel disease. *J Cereb Blood Flow Metab* (2017) 37(2):644–56. doi:10.1177/0271678X16635857
10. Li Y, Li M, Zhang X, Shi Q, Yang S, Fan H, et al. Higher blood-brain barrier permeability is associated with higher white matter hyperintensities burden. *J Neurol* (2017) 264(7):1474–81. doi:10.1007/s00415-017-8550-8
11. Wardlaw M, Doubl FN, Valdes-Hernandez M, Wang X, Chappell FM, Shuler K, et al. Blood-brain barrier permeability and long-term clinical and imaging outcomes in cerebral small vessel disease. *Stroke* (2013) 44(2):525–7. doi:10.1161/STROKEAHA.112.669994
12. Staals J, Makin SD, Doubal FN, Dennis MS, Wardlaw JM. Stroke subtype, vascular risk factors, and total MRI brain small-vessel disease burden. *Neurology* (2014) 83(14):1228–34. doi:10.1212/WNL.0000000000000837

13. Yang Y, Rosenberg GA. Blood-brain barrier breakdown in acute and chronic cerebrovascular disease. *Stroke* (2011) 42(11):3323–8. doi:10.1161/STROKEAHA.110.608257

14. Lavini C, Verhoeff JJ. Reproducibility of the gadolinium concentration measurement and of the fitting parameters of the vascular input function in the superior sagittal sinus in a patient population. *Magn Reson Imaging* (2010) 28(10):1420–30. doi:10.1016/j.mri.2010.06.017

15. van de Haar HJ, Jansen JFA, Jeukens C, Burgmans S, van Buchem MA, Muller M, et al. Subtle blood-brain barrier leakage rate and spatial extent: considerations for dynamic contrast-enhanced MRI. *Med Phys* (2017) 44(8):4112–25. doi:10.1002/mp.12328

16. Cramer SP, Simonsen H, Frederiksen JL, Rostrup E, Larsson HB. Abnormal blood-brain barrier permeability in normal appearing white matter in multiple sclerosis investigated by MRI. *Neuroimage Clin* (2014) 4:182–9. doi:10.1016/j.neiclin.2013.12.001

17. Fazekas F, Chawluk JB, Alavi A, Hurtig HI, Zimmerman RA. MR signal abnormalities at 1.5 T in Alzheimer’s dementia and normal aging. *AJR Am J Roentgenol* (1987) 149(2):351–6. doi:10.2214/ajr.149.2.351

18. Gregoire SM, Chaudhury UJ, Brown MM, Yousry TA, Kallis C, Jager HR, et al. The Microbleed Anatomical Rating Scale (MARS): reliability of a tool to map brain microbleeds. *Neurology* (2009) 73(21):1759–66. doi:10.1212/WNL.0b013e3181c34a7d

19. Doubal FN, MacLullich AM, Ferguson KJ, Dennis MS, Wardlaw JM. Stroke subtype, vascular risk factors, and total MRI brain small-vessel disease burden. Data from the third international stroke trial. *J Stroke Cerebrovasc Dis* (2017) 26(7):1506–13. doi:10.1016/j.jstrokecerebrovasdis.2017.03.002

20. Poels MM, Vernooy MJ, Ikram MA, Hofman A, Krestin GP, van der Lugt A, et al. Prevalence and risk factors of cerebral microbleeds: an update of the Rotterdam scan study. *Stroke* (2010) 41(10 Suppl):S103–6. doi:10.1161/STROKEAHA.110.595181

21. Schreiber S, Buche C, Garz C, Braun H. Blood-brain barrier breakdown as the starting point of cerebral small vessel disease? – new insights from a rat model. *Exp Transl Stroke Med* (2013) 5(1):4. doi:10.1186/2040-7378-5-4

22. Zhao Z, Nelson AR, Betsholtz C, Zlokovic BV. Establishment and dysfunction of the blood-brain barrier. *Cell* (2015) 163(5):1064–78. doi:10.1016/j.cell.2015.10.067

23. Hainsworth AH, Fisher M J. A dysfunctional blood-brain barrier and cerebral small vessel disease. *Neurology* (2017) 88(5):420–1. doi:10.1212/WNL.0000000000003561

24. Muller K, Courtois G, Ursini MV, Schwaninger M. New insight into the pathogenesis of cerebral small-vessel diseases. *Stroke* (2017) 48(2):520–7. doi:10.1161/STROKEAHA.116.012888

25. Rosenberg GA, Wallin A, Wardlaw JM, Markus HS, Montaner J, Wolfson L, et al. Consensus statement for diagnosis of subcortical small vessel disease. *J Cereb Blood Flow Metab* (2016) 36(1):6–25. doi:10.1038/jcbfm.2015.172

26. Craggs LJ, Yamamoto Y, Deramecourt V, Kalaria RN. Microvascular pathology and morphometrics of sporadic and hereditary small vessel diseases of the brain. *Brain Pathol* (2014) 24(5):495–509. doi:10.1111/bpa.12177

27. Cordonnier C, van der Flier WM. Brain microbleeds and Alzheimer’s disease: innocent observation or key player? *Brain* (2011) 134(Pt 2):335–44. doi:10.1093/brain/awq321

28. Valdes Hernandez M, Allerhand M, Glatz A, Clayton L, Munoz Maniega S, Gow A, et al. Do white matter hyperintensities mediate the association between brain iron deposition and cognitive abilities in older people? *Eur J Neurol* (2016) 23(7):1202–9. doi:10.1111/ene.13006

29. Arba E, Mair G, Carpenter T, Sakka E, Sandecky PAG, Lindley RJ, et al. Cerebral white matter hyperperfusion increases with small-vessel disease burden. *Stroke* (2014) 45(6):1633–6. doi:10.1177/0039249913507301

30. Shi Y, Thrippleton MJ, Makin SD, Marshall I, Greerings MI, de Craen AJ, et al. Cerebral blood flow in small vessel disease: a systematic review and meta-analysis. *J Cereb Blood Flow Metab* (2016) 36(10):1653–67. doi:10.1177/0271678X1662891

31. ten Dam VH, van den Heuvel DM, de Craen AJ, Bollen EL, Murray HM, Westendorp RG, et al. Decline in total cerebral blood flow is linked with increase in periventricular but not deep white matter hyperintensities. *Radiology* (2007) 243(1):198–203. doi:10.1148/radiol.2431052111

32. Maniega SM, Valdes Hernandez MC, Clayden JD, Royle NA, Murray C, Morris Z, et al. White matter hyperintensities and normal-appearing white matter integrity in the aging brain. *Neurobiol Aging* (2015) 36(2):909–18. doi:10.1016/j.neurobiolaging.2014.07.048

**Conflict of Interest Statement:** Author QS was employed by company Siemens Healthcare Ltd. All other authors declare no competing interests.

Copyright © 2018 Li, Li, Zuo, Shi, Qiu, Yang, Jiang and Hu. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.