Biomechanical Study of Posterior Pelvic Fixations in Vertically Unstable Sacral Fractures: An Alternative to Triangular Osteosynthesis

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Study Design: Biomechanical study.
Purpose: To investigate the relative stiffness of a new posterior pelvic fixation for unstable vertical fractures of the sacrum.
Overview of Literature: The reported operative fixation techniques for vertical sacral fractures include iliosacral screw, sacral bar fixations, transiliac plating, and local plate osteosynthesis. Clinical as well as biomechanical studies have demonstrated that these conventional techniques are insufficient to stabilize the vertically unstable sacral fractures.
Methods: To simulate a vertically unstable fractured sacrum, 12 synthetic pelvic models were prepared. In each model, a 5-mm gap was created through the left transforaminal zone (Denis zone II). The pubic symphysis was completely separated and then stabilized using a 3.5-mm reconstruction plate. Four each of the unstable pelvic models were then fixed with two iliosacral screws, a tension band plate, or a transiliac fixation plus one iliosacral screw. The left hemipelvis of these specimens was docked to a rigid base plate and loaded on an S1 endplate by using the Zwick Roell z010 material testing machine. Then, the vertical displacement and coronal tilt of the right hemipelvis and the applied force were measured.
Results: The transiliac fixation plus one iliosacral screw constructions could withstand a force at 5 mm of vertical displacement greater than the two iliosacral screw constructions ($p=0.012$) and the tension band plate constructions ($p=0.003$). The tension band plate constructions could withstand a force at 5° of coronal tilt less than the two iliosacral screw constructions ($p=0.027$) and the transiliac fixation plus one iliosacral screw constructions ($p=0.049$).
Conclusions: This study proposes the use of transiliac fixation in addition to an iliosacral screw to stabilize vertically unstable sacral fractures. Our biomechanical data demonstrated the superiority of adding transiliac fixation to withstand vertical displacement forces.
Keywords: Sacrum; Fracture fixation; Biomechanics; Iliosacral screw; Triangular osteosynthesis

Introduction
Operative treatment is often required for unstable sacral fractures. Treating unstable fracture located in the posterior pelvic ring requires consideration of the stability of the region into account. An unstable sacral fracture with posterior pelvic ring disruptions can result in rotational and vertical instability of the pelvis. The current operative
techniques include iliosacral screw, sacral bar fixations, transiliac plating, and local plate osteosynthesis [1-4]. However, clinical and biomechanical studies have demonstrated that these conventional techniques are often insufficient to stabilize vertically unstable sacral fractures [5-8].

Kach and Trentz [9] described a technique called distraction spondylodesis to counter the vertical shear forces existing in vertically unstable sacral fracture zones II and III (Denis) [10]. This technique involves a transfixation from L5 to the pelvic rim without any direct fixation across the fracture site. In another study, Schildhauer et al. [11] introduced the use of triangular osteosynthesis. This fixation was a variation of the technique described earlier by Kach and Trentz [9]. Schildhauer et al. [11] used a supplemental iliosacral screw to maintain sacral fracture reduction (Fig. 1). Another biomechanical study concluded that triangular osteosynthesis was superior to iliosacral screw fixation [7]. Patients with former fixation are allowed to undertake early progressive weight-bearing activities [11,12]. However, the drawback of this technique is the need for fixation across the L5 to S1 or even L4 to S1 motion segments, thereby leading to loss of motion and/or possible chronic back pain [13,14].

As a potentially superior option to triangular osteosynthesis, we devised a technique involving transiliac fixation with iliosacral screw fixation for vertically unstable sacral fractures. The transiliac fixation could reinforce the iliosacral screw without touching the lumbosacral motion segment. The purpose of this study was to ascertain biomechanical advantage of adding a transiliac fixation in case of vertically unstable sacral fractures.

**Materials and Methods**

This work was a biomechanical investigation of synthetic pelvic models. After obtaining approval from the institutional review board of Human Research Ethics Committee, Faculty of Medicine, Prince of Songkla University (IRB approval no., REC 58-057-11-1), 12 synthetic pelvic models (Pacific Research Laboratories Inc., Vashon, WA, USA) were prepared to simulate the vertically unstable fractured sacrum. In each model, a 5-mm gap was created through the left transforaminal zone (Denis zone II). The pubic symphysis was completely separated and then stabilized using a 3.5-mm reconstruction plate. Four each of the unstable pelvic models were fixed with (1) two iliosacral screws, (2) a tension band plate, or (3) a transiliac fixation plus one iliosacral screw (Fig. 2). A fully threaded cancellous screw (6.5 mm in diameter, 90 mm in length) was employed as the iliosacral screw. An appropriately sized 15-hole reconstruction plate with 3.5-mm cortical screws was used as the posterior tension band plate. Transiliac fixation consisted of one 8.0×100-mm monoaxial pedicle screw inserted into each ilium at the posterior superior iliac spine. The screw was inserted through the dense bone above the superior aspect of the sciatic notch, and the screws present in both the ilia were connected using a 6.0-mm rod. To simulate a single-leg stance model, the
left hemipelvis of all the models was docked to a rigid base plate modified from the Moore’s prosthesis. Distance (HC-SR04) and gyro (UM7 Orientation Sensor) sensors were then installed into the right hemipelvis to detect the vertical displacement and coronal tilt, respectively. Each specimen was vertically loaded onto an S1 endplate by using the Zwick Roell z010 material testing machine (Zwick, Ulm, Germany) (Fig. 3). Prior testing with a static load of 10 mm/min on each pelvic model demonstrated that the two iliosacral screw constructions, tension band plate construction, and transiliac fixation plus one iliosacral screw construction could withstand a maximum vertical load of 280 N, 161 N, and 510 N, respectively. Therefore, the loading sequences were started with a cyclical preload (25 cycles, 120 mm/min) up to 30% of the maximum withstandable force in each construction type, followed by a subsequent static load of 10 mm/min. During the loading process, vertical displacement and the coronal tilt of the right hemipelvis along with applied force were measured.

The normality of the data was confirmed with the Shapiro–Wilk and Kolmogorov–Smirnov tests. One-way analysis of variance was used to determine the force for displacement between the pelvic constructions. Post hoc test was applied for multiple comparisons. All statistical analyses were conducted using SPSS ver. 17.0 (SPSS Inc., Chicago, IL, USA). A $p<0.05$ was considered statistically significant.

**Results**

1. **Vertical displacement**

The mean values of force (N) required for 5-mm vertical displacement of the right hemipelves are shown in Table 1. The transiliac fixation plus one iliosacral screw construction could withstand a force (mean, 286.8 ± 53.2) at 5 mm of vertical displacement greater than the two iliosacral screws ($p=0.012$) and the tension band plate ($p=0.003$) constructions. No statistically significant differences were observed in the force required for 5-mm vertical displac-

| Table 1. Force (N) at 5 mm vertical displacement |
|--------------------------------------------------|
| **Fixation type** | **Mean±standard deviation** |
| Two ISS | 152.51±42.48 |
| Tension band plate | 118.42±57.13 |
| Transiliac fixation+one ISS | 286.82±53.21 |

| Table 2. Multiple comparisons of force (N) for 5 mm vertical displacement |
|--------------------------------------------------------------------------|
| **Fixation type (1)** | **Fixation type (2)** | **Mean difference (1)–(2)** | **p-value** |
| Two ISS | Tension band plate | 34.08 | 0.631 |
| | Transiliac fixation+one ISS | -134.31 | 0.012* |
| Tension band plate | Two ISS | -34.08 | 0.631 |
| | Transiliac fixation+one ISS | -168.39 | 0.003* |
| Transiliac fixation+one ISS | Two ISS | 134.31 | 0.012* |
| | Tension band plate | 168.39 | 0.003* |

ISS, iliosacral screw.
*Statistically significant if $p<0.05$.
ment between the two iliosacral screws and the tension band plate \((p=0.631)\) constructions (Table 2).

2. Coronal angulation

The mean values of force (N) required for 5° of coronal tilt of the right hemipelves are listed in Table 3. The tension band plate construction could withstand only a lesser force at 5° of coronal tilt than the two iliosacral screws \((p=0.027)\) and the transiliac fixation plus one iliosacral screw \((p=0.049)\) constructions. The forces required to achieve 5° of coronal tilt were not significantly different between the two iliosacral screws and the transiliac fixation plus one iliosacral screw \((p=0.926)\) constructions (Table 4).

**Table 3. Force (N) at 5° coronal tilt**

| Fixation type                  | Mean±standard deviation |
|-------------------------------|-------------------------|
| Two ISS                       | 761.02±290.53           |
| Tension band plate            | 329.91±108.98           |
| Transiliac fixation+one ISS   | 710.11±117.62           |

ISS, iliosacral screw.

**Table 4. Multiple comparisons of force (N) for 5° coronal tilt**

| Fixation type (1) | Fixation type (2) | Mean difference (1)–(2) | \(p\)-value |
|-------------------|-------------------|-------------------------|-------------|
| Two ISS           | Tension band plate| 431.11                  | 0.027*      |
|                   | Transiliac fixation+one ISS | 50.90                | 0.926       |
| Tension band plate| Two ISS           | -431.11                 | 0.027*      |
|                   | Transiliac fixation+one ISS | -380.20               | 0.049*      |
| Transiliac fixation+one ISS | Two ISS         | -50.90                  | 0.926       |
|                   | Tension band plate | 380.20                  | 0.049*      |

ISS, iliosacral screw.

*Statistically significant if \(p<0.05\)

Discussion

The sacrum is unique in terms of its anatomical and mechanical aspects [15-17], and fractures in this region need specific attention. Anatomical restrictions for instrumental fixation, neural tissue proximity, and high axial load bearing pose difficulties in fracture fixation [15,18,19]. The iliosacral screw is one of the conventional methods for treating a vertical fracture in the sacrum. Griffin et al. [6] reported 13% failure rate with the use of a percutaneous iliosacral screw in treating unstable pelvic fractures. The researchers established that the failures were not associated with any specific surgical techniques, rather only with the presence of a vertical sacral fracture. Keating et al. [5] analyzed the outcomes of vertically unstable pelvises treated with iliosacral screw fixation. The study reported a malunion rate of 56% and suggested augmentation with a rigid anterior fixation to minimize this occurrence. Triangular osteosynthesis, a combination of iliosacral fixation and ipsilateral lumbopelvic fixation, was originally introduced by Schildhauer et al. [11]. The problem addressed in this research was the rotational and vertical instability resulting from vertically unstable sacrum fractures. Thus, to achieve adequate stability, both transverse (iliosacral) and vertical (lumbopelvic) fixations are required to control rotational and vertical instability, respectively. One biomechanical study ascertained that an additional unilateral lumbopelvic fixation provided better stability than iliosacral screw fixation alone [7]. This result implies that lumbopelvic fixation can protect iliosacral screw and reduce the failure rate when treating patients with vertically unstable sacral fractures [6,20]. However, triangular osteosynthesis comes with certain disadvantages. Sagi et al. [13,14] reported drawbacks including delayed union, non-union, and lumbosacral scoliosis with chronic low back pain.

As the sacrum is a part of the posterior pelvic ring and the intercalary bone between the spine and the pelvis, a fracture may cause spinopelvic dissociation wherein there is a disconnection between the cephalad lumbar spine/central sacrum and the caudad bilateral sacral alae [21,22]. In this situation, a spinopelvic fixation, which is a bilateral lumbopelvic fixation without or with iliosacral fixation, is required to transmit the load from the spine to the ilium bilaterally [22,23]. In cases of spinopelvic dissociation, it is reasonable to perform a fixation at the expense of lower
lumbar motion. However, in cases of vertical sacral fracture without spinopelvic dissociation, iliosacral fixation plus ipsilateral lumbopelvic fixation (triangular osteosynthesis) appears to be unwarranted. Thus, instead of resorting to triangular osteosynthesis in these cases, we have suggested the use of a transiliac fixation for enhancing the iliosacral screw fixation.

The issues regarding whether cadaver or synthetic bone is more suitable for biomechanical testing remains controversial. The cadaveric pelvis is closer to a normal human pelvis; the inter-specimen variation is a concern. Furthermore, the mechanical properties of new generation synthetic bones are comparable to those of human specimens [24,25]. Our biomechanical study on synthetic pelvic models revealed the superiority of adding transiliac fixation for resisting vertical displacement over the use of iliosacral screw fixation alone (Table 2). Moreover, we observed that transiliac fixation was stiffer than iliosacral screw fixation alone, and hence, capable of resisting coronal tilt (Table 4). These data may encourage the usage of a transiliac fixation to supplement an iliosacral screw in case of vertically unstable sacral fractures, leaving the lumbar spine untouched.

This study, however, has several limitations. We did not compare the transiliac fixation construction with triangular osteosynthesis directly for two reasons. First, a synthetic pelvic model incorporating the lumbar spine was not available. Second, we did not consider the transverse (transiliac) fixation to be stronger than the vertical (triangular osteosynthesis) fixation in terms of vertical stability. However, we did not aim for the strongest fixation; we aimed for a strong enough fixation that leaves the lumbar spine undisturbed. Furthermore, this work was a biomechanical study involving synthetic bone; hence, we did not include the reinforcement from the soft tissues. Moreover, the research may not be able to predict the adverse outcomes in clinical situations, such as hardware prominence, nonunion, and future adverse radiographic sequelae. The ability of the transiliac fixation to supplant the triangular osteosynthesis requires further clinical studies.

**Conclusions**

We have proposed the use of a transiliac fixation to supplement the iliosacral screw. This approach should minimize the failure rate of iliosacral screws in treating vertically unstable sacral fractures. We believe that the proposed transiliac fixation plus iliosacral screw construction can serve as a good alternative to triangular osteosynthesis while simultaneously reducing the undesired consequences of lumbopelvic fixation. As a biomechanical study, however, the clinical benefits remain to be proven.

**Conflict of Interest**

No potential conflict of interest relevant to this article was reported.

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