Modification of fliposomes with a polycation can enhance the control of pH-induced release

Anastasia Yu Lokova
Olga V Zaborova
Department of Chemistry, M.V. Lomonosov Moscow State University, 119991 Moscow, Russian Federation

Purpose: Nowadays, the development of stimuli-sensitive nanocontainers for targeted drug delivery is of great value. Encapsulation of a drug in a pH-sensitive liposomal container not only provides protective and transport functions, but also helps to create a system with a controlled release mechanism.

Methods: In this study, we investigated the influence of a cationic polypeptide on the pH-induced release of anticancer drug doxorubicin (DXR) from the anionic fliposomes – liposomes consisting of a neutral lipid, an anionic lipid (prone to interact with a polycation), and a lipid trigger (impacting the pH-sensitivity).

Results: First, we showed the possibility to control the pH-induced release by the simple modification of the anionic fliposomes with linear polylysine. Second, we optimized the fliposomal composition such that the obtained fliposomes responded to the pH changes only when complexed with the polycation (“turning on” the release). Finally, pH-induced release from the polylysine-modified anionic fliposomes was tested on an anticancer drug DXR.

Conclusion: We have succeeded in developing “smart” stimuli-sensitive nanocontainers capable of tunable controlled release of a drug. Moreover, based on the data on release of a low molecular salt, one can predict the release profile of DXR.

Keywords: polylysine, polymer–colloid complex, stimuli-sensitive nanocontainer, pH-sensitivity, controllable drug release

Introduction

The development of nanocontainers for the delivery of biologically active compounds has attracted considerable attention for its potential application in pharmacology. The encapsulation of biologically active compounds can bring a variety of benefits including a reduction in the side effect and an increase in the bioavailability of substances. Polymeric micelles, nanoemulsions, and liposomes are amongst the most studied systems to develop such containers. However, despite a significant progress in the design of liposomal nanocontainers, only a few of them are available on the market, mainly due to the low therapeutic effect of the liposomal formulations which is directly related to the low efficiency of drug release. It has been recognized now that the targeted release of the encapsulated compound is one of the approaches to increase the therapeutic efficiency, as a result of the environmental changes in the infected tissue such as pH, redox potential, enzyme activity, etc. For example, the tumor extracellular pH is slightly acidic in comparison to the blood pH, thus the containers capable of releasing the drug in response to a decrease of pH are of great interest. The vast majority of the pH-sensitive liposomal agents are weak acids or acid-hydrolyzed lipid derivatives, including the most widely used pH-sensitive liposomes with phosphatidylethanolamine (PE) and the complementary lipid,
accessible for protonation. The complementary lipid stabilizes the mixed bilayer membrane at neutral pH, whereas it becomes protonated and immiscible with the PE molecules after decrease in pH resulting in disruption of the liposomes and formation of individual vesicles and hexagonal phase of PE lipids. Another method to prepare the pH-sensitive liposomes is to use molecules possessing weak acidic properties, for example, cholesteryl hemisuccinate (CHEMS), which has a negative charge at neutral pH and thus ensures the aggregative stability of the liposomes. Decrease of pH leads to the neutralization of the CHEMS molecule and causes the liposomal aggregations and the release of the encapsulated compound.

Polyelectrolytes, such as polyacrylic acid or carboxylated hyaluronic acid, have also been used as pH-sensitive agents for liposomes, as they become hydrophilic with the decrease of pH value and, thus, disrupt a liposomal membrane. The formation of sterically stabilized polyethylene glycol (PEG)–phenyl vinyl ether (PIVE)–lipid conjugate liposomes was recently reported. The acid-labile bond between PEG and PIVE lipid derivative cleaves under the acidic conditions, resulting in the loss of stability effect, liposome aggregation, and the release of content.

Conformational switches are another class of pH-sensitive liposomal agents that are represented by quasi-lipids based on cyclohexane, piperidine, or bispidinone. Trans-4,5-didodecyloxycarbonyl-2-morpholinocyclohexanol (TR)-based lipid is reported to belong to this class of agents and is the most promising for biomedical applications. Protonation leads to the formation of a hydrogen bond between morpholine and hydroxyl groups resulting in the conformational flip of a cyclohexanol ring and, finally, to the disruption of the liposomal membrane and the release of the encapsulated compound. The liposomes containing this type of a lipid molecule are called “fliposomes.” The pH-induced conformational flip of TR is presented in Figure 1.

This study aimed to develop a tunable pH-sensitive liposomal container for the encapsulation and controlled release of the anticancer drug doxorubicin (DXR). We investigated the possibility of controlling the pH-induced release of the encapsulated compounds by simple modification of fliposomes by using a linear biocompatible polycation. Previously, we studied the interaction of branched polycations (brush-like or star-shaped) with anionic fliposomes and showed an increase in the rate and amount of the content release. However, the adsorption of the branched polycations induces the transmembrane migration (flip-flop) of the anionic lipids from the inner to the outer layer of a liposomal membrane, thus causing the formation of undesirable defects inside the membrane and limiting the application of such constructions for drug delivery. We decided to use linear polylysine, to prevent the formation of the undesirable defects upon adsorption of the polycation on the surface of anionic fliposomes as this polymer does not induce flip-flop of the anionic lipids. Moreover, polylysine is capable of undergoing enzymatic degradation due to its polypeptide structure and can also be used as a model to mimic blood proteins.

Materials and methods

Materials

α-Polylysine hydrobromide (pLys) with a chain length of 70 units (MW = 15,000 g/mol) was purchased from Sigma Aldrich Co. (St Louis, MA, USA). Polylysine concentration is given as number of moles of the repeating units per liter. 1,2-Dioleoyl-sn-glycerol-3-phosphocholine (PC), 1-palmitoyl-2-oleoyl-sn-glycero-3-phospho-L-serine (PS), and 1,2-dioleoyl-sn-glycerol-3-phosphoethanolamine-N-(lissamine rhodamine B sulfonyl) (PE-Rhod) were purchased from Avanti Polar Lipids Inc (Alabaster, AL, USA). The chemical structures of the lipids used in the study are presented in Figure 2. TR (lipid trigger) was synthesized in N.D. Zelinsky Institute of Organic Chemistry by Vasily Migulin as described elsewhere.

The buffer solutions used were as follows: Tris buffer (HOCH$_2$)$_3$CNH$_2$, 1 mmol/L, pH 7.4; phosphate buffer (Na$_2$HPO$_4$, NaH$_2$PO$_4$, NaCl), 10 mmol/L, pH 7.4; acetate buffer (CH$_3$COOH, CH$_3$COONa), 1 mmol/L, pH 5.5.
Methods
Preparation of liposomes
Small monolamellar liposomes were prepared using the standard procedure. Briefly, the required amounts of lipids were dissolved in chloroform. Then the organic solvent was removed under vacuum (Rotavapor; Buchi, Flawil, Switzerland) at 36°C. A thin lipid film was dispersed in a buffer solution. Then the dispersion was sonicated using a titanium probe for 2×300 seconds (Ultrasonic homogenizer 4710; Cole-Parmer, Niles, IL, USA). Obtained liposomes were centrifuged (Centrifuge J-11; Beckman, Palo Alto, CA, USA) for 5 minutes at 11,000 rpm to separate from titanium dust. The molar ratio of the lipids PS/TR/PC in the liposomes formed was 1/3/6 (fliposomes 1), 3/0.5/6.5 (fliposomes 2), and 3/1/6 (fliposomes 3). The lipid content, effective diameter \(D_{\text{eff}}\), and the electrophoretic mobility (EPM) of the fliposomal formulations used in 1 mmol/L Tris buffer solution, pH 7.4, are presented in Table 1. The obtained liposomal suspension was stored at 4°C and used within 3 days.

Fluorescent-labeled liposomes were prepared using the same procedure, except that 0.5 wt% of PE-Rhod lipid (Figure 2) was added to the lipid mixture solution before chloroform evaporation.

NaCl-loaded liposomes were prepared by dispersing the lipid film in 1 M NaCl solution followed by the dialysis of the liposomal suspension against water as described previously.

| Sample code | PS, molar% | TR, molar% | PC, molar% | \(D_{\text{eff}}\), nm | EPM, \((\mu\text{m/s})/(V/cm)\) |
|-------------|------------|------------|------------|----------------------|---------------------------------|
| Fliposomes 1 | 10         | 30         | 60         | 100.3±9.1             | −2.73±0.10                      |
| Fliposomes 2 | 30         | 5          | 65         | 73.6±5.7              | −3.53±0.11                      |
| Fliposomes 3 | 30         | 10         | 60         | 87.4±6.2              | −3.46±0.13                      |

Abbreviations: \(D_{\text{eff}}\), effective hydrodynamic diameter; EPM, electrophoretic mobility; PS, 1-palmitoyl-2-oleoyl-sn-glycero-3-phospho-L-serine; PE-Rhod, 1,2-dioleoyl-sn-glycero-3-phosphethanolamine-N-(lissamine rhodamine B sulfonyl); TR, trans-4,5-didodecylloxy-carbonyl-2-morpholinocyclohexan.
The obtained NaCl-loaded liposomes were stored at 4°C and used within 2 days.

Ammonium sulfate gradient liposomes for the DXR loading were prepared by dispersing the lipid film in 100 mmol/L (NH₄)₂SO₄ solution and then dialyzing against PBS (10 mmol/L, pH=7.4). The DXR solution was added to the liposomal suspension in the ratio lipid/DXR =10/1 (w/w). The unloaded DXR was separated via Sepharose G-25 column using PBS as eluent. Liposomal suspension was stored at 4°C and used within 1 day.

Dynamic light scattering (DLS)
Effective diameters of liposomes and their complexes with polylysin were determined by DLS in a thermostated cell with a Brookhaven Zeta Plus instrument (New York, NY, USA). The intensity of the scattered light was detected at the angle θ=90° using a laser with a wavelength of 640 nm. DLS data were evaluated using the software provided by the manufacturer. The values were the average of at least three independent measurements.

Microelectrophoresis
The EPM was measured by laser microelectrophoresis technique using the same Brookhaven Zeta Plus instrument used for DLS measurements. The software provided by the manufacturer was used to calculate the EPM of the samples. Each mobility value presented in the text is an average of ten values.

Fluorescence
The fluorescence intensity of rhodamine-labeled liposome suspensions was measured at λ_{em} = 571 nm (λ_{ex} = 557 nm) using F-4000 Hitachi fluorescence spectrophotometer (Hitachi, Japan). The release of DXR was monitored using F-4000 Hitachi fluorescence spectrophotometer (λ_{em} = 555 nm, λ_{ex} = 490 nm). The cell temperature was maintained constant at 25°C±0.1°C or 37°C±0.1°C.

Conductometry
The NaCl release was monitored by measuring the conductivity of the NaCl-loaded vesicle suspensions in a buffer solution with a CDM83 conductometer (Radiometer, Copenhagen, Denmark). The cell temperature was maintained constant at 25°C±0.1°C or 37°C±0.1°C.

Potentiometry
The pH values of buffer solutions were determined using the pH-meter 210 (Hanna, Woonsocket, RI, USA) with a glass electrode HI 1131B.

Results and discussion
First, the dependence of the degree of protonation of polylysine amino groups (α) as a function of pH was investigated using the method described previously. Polylysine is a weak base with a theoretical pKₐ2 value about 10.44, thus a 0.4 mM water solution of pLys was converted into a free-base form by addition of an equimolar amount of NaOH and titrated with 0.1 M HCl solution. The equivalence point obtained from the titration curve (Figure 3A) was at pH=6.77. The pH dependence of α values was calculated as the second step based on the potentiometric titration data (Figure 3B).

The interaction of polylysine with anionic fliposomes was studied further at pH 7.4 which corresponds to almost fully protonated form of the polycation.

Complexation of fliposomes 1 with linear polylysine
Addition of polylysine to the suspension of anionic fliposomes 1 led to the decrease of surface charge of the particles due to the formation of the polycation–liposomal electrostatic complex (Figure 4, curve 1). The complex formation was followed by the laser microelectrophoresis technique.

As one can see from Figure 4, the concentration of polylysine needed for the neutralization of the total surface charge of forming complexes was 0.056 mmol/L which corresponds to the anionic lipid/cationic groups ratio, [-]/[+] =2, suggesting that only a half of the anionic lipids present in the system interacted with polylysine. It was argued earlier that lipids are distributed uniformly between the inner and outer leaflets in the model membranes. Thus, the formation of the neutral complex at [-]/[+] =2 implies that polylysine interacts with the anionic lipids located only on the outer leaflet of the liposomal membrane. In other words, the adsorption of polylysine does not induce a flip-flop of anionic lipids, which is consistent with the previously published data. Further addition of polylysine resulted in the sign change of the EPM of particles. The size measurements of the complexes showed a common behavior for the poliyon-decorated vesicles connected with the re-entrant condensation: the complex size increased with the approach of the particle charge neutralization point and size decrease after passing the charge inversion point (Figure 4, curve 2). The complexes with the excess of polylysine ([−]/[+]<1) were colloidally stable with surface charge value of 1.5 (μm/s)/(V/cm) and had the size of the initial liposomes.

Once the complex is formed, its association–dissociation stability should depend on the ionic strength of the media. The complex stability was evaluated by the titration of fluorescently-labeled fliposomes with polylysine solution. Formation of the complex led to the decrease of fluorescence intensity.
Figure 3 (A) Potentiometric titration of a 0.4 mM pLys water solution with 0.1 M HCl solution. (B) Dependence of the degree of pLys amino group protonation (α) on pH value. Abbreviations: pLys, α-polylysine hydrobromide; eq, equivalent.

The formation of complexes was investigated at two different pH values corresponding to the pH of healthy tissues (pH=7.4, Tris buffer) and tumors (pH=5.5, acetate buffer). Figure 5A shows that the change in pH did not change the nature of the interaction between polylysine and anionic fliposomes, although the lipid trigger was partially protonated at pH=5.5. Nevertheless, we observed some differences in the salt concentration required for complex dissociation (Figure 5B). At pH 7.4, the complex was stable up to 0.2 M NaCl (Figure 5B, curve 1), while the complex started to dissociate at NaCl concentration higher than 0.05 M at pH 5.5 (Figure 5B, curve 2). The complex formed initially at pH 7.4 and when transferred to pH 5.5 (Figure 5B, curve 3) had the same stability as the complex formed at pH 5.5. Such differences in the NaCl concentration needed for complex dissociation (pH=7.4 and pH=5.5 could be attributed to 1) different [-]/[+] ratios of the complexes titrated by NaCl solution – 1 and 0.77 for complexes formed at pH=7.4 and 5.5, respectively; 2) partial protonation of lipid trigger that facilitates the complex dissociation; and 3) probable influence of the nature of buffer ions on the dissociation of complexes. Nevertheless, the influence of the ionic strength on the dissociation stability of anionic fliposomes/polylysine complexes is out of scope of the current research.

Tunable pH-induced release – acceleration of the release rate (fliposomes 1)

The pH-induced release of the encapsulated hydrophilic compound was investigated using the NaCl-loaded fliposomes. The complexes with excess of polylysine ([−]/[+] =0.5) were used. The salt release was followed conductometrically46 at two different temperatures: 25°C (Figure 6A) and 37°C.
(Figure 6B). The control experiments at both temperatures (Figure 6, curve 3) showed that the adsorption of polylysine at pH 7.4 does not disturb the lipid membrane and thus does not lead to the release. The suspension of individual fliposomes or the complex formed at pH 7.4 was transferred to the buffer solution with pH 5.5 and the conductivity was monitored at different time intervals. The measured values were normalized to the conductivity of the system treated with Triton X-100; this state was attributed to the complete rupture of the fliposomes.

The change in pH induced the immediate onset of the release of contents from both the individual fliposomes

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**Figure 5** (A) Relative fluorescence intensity of labeled fliposomes 1 (cf Methods section) vs polylysine concentration, pH=7.4 (1) and pH=5.5 (2). (B) Changes in the relative fluorescence intensity of labeled fliposomes 1 complex with polylysine after NaCl addition. Complex formed at pH=7.4 with [-]/[+] =1 (1), at pH=5.5 with [-]/[+] =0.77 (2), and complex formed at pH=7.4 with [-]/[+] =1 and titrated with NaCl at pH=5.5 (3). C_{lip}=0.73 mg/mL (C_{anionic}=0.1 mmol/L), T=25°C.

**Abbreviation:** pLys, α-polylysine hydrobromide.

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**Figure 6** Time-dependent pH-induced release for individual fliposomes 1 (curves 1 and 3) and fliposomes 1 in complex with polylysine with [-]/[+] =0.5 (curves 2 and 4) at pH=5.5 (curves 1 and 2) and pH=7.4 (curves 3 and 4). T=25°C (A) and 37°C (B). C_{lip}=1 mg/mL (C_{anionic}=0.14 mmol/L).
Composition optimization (fliposomes 2 and 3)

We prepared the fliposomes with altered composition to investigate whether it is possible to make fliposomal container responsive to the pH decrease only in a complex with polycations. The content of anionic liposomal container was increased to a molar fraction of 30% to enhance the effect of lateral concentration of anionic lipids induced by the polycation. It was previously shown that the increase of the amount of anionic lipid up to the molar fraction of 30% improves the stability of the polycation–liposome complex in water-salt media, although the liposomal structure is not still disrupted under the adsorption of the polycation. Two molar fractions of lipid trigger were used: 5% for fliposomes 2 and 10% for fliposomes 3 to suppress the release from the individual fliposomes after decreasing of pH (Table 1).

The changes in the surface charge and size of particles are presented in Figure 7 as a function of the polylysine concentration. The neutralization of the fliposomal surface charge occurred at the concentration of 0.11 mmol/L of added polylysine both for the systems with fliposomes 2 (Figure 7A, curve 1) and fliposomes 3 (Figure 7B, curve 3). This amount corresponded to the [-1]t[+]=2 and was attributed to the absence of flip-flop of the anionic lipid similar to fliposomes 1.

The stability of the liposome/polylysine complex in water-salt media was evaluated as described for the system with fliposomes 1 (Figure 5). The addition of polylysine solution to the suspension of anionic fliposomes 3 led to complex formation irrespective of the pH of media (Figure 8A). The complexes were stable up to a salt concentration of 0.2 M (Figure 8B). The data for the fliposomes 2 system are not presented as they are identical to the data for the fliposomes 3 system (Figure 8). We conclude that the complexes of fliposomes 3 with polylysine seemed to be more stable in water-salt media than complexes of fliposomes 1. An increase in the stability of the anionic liposome–polycation complexes with the increase of the molar fraction of anionic lipid was also observed for the systems with branched polycations.

Tunable pH-induced release – “turning on” the release (fliposomes 2 and 3)

The pH-induced release was tested on the fliposomes 2 and fliposomes 3 loaded with 1 M NaCl both for individual
liposomes and liposomes in complex with the excess of polycation at two temperatures: 25°C and 37°C. The leakage from individual liposomes 2 was about 0.03 after 2 hours of pH change at both temperatures (Figure 9, curve 1). The liposomes 2 in complex with polycation released the encapsulated salt up to 0.04 and 0.06 at 25°C and 37°C, correspondingly (Figure 9, curve 2). The individual liposomes 3 did not leak after pH change at 25°C (Figure 9A, curve 3), while there was a negligible release up to 0.03 at 37°C (Figure 9B, curve 3). We regard the salt leakage of 0.05 as negligible as it was comparable with the instrumental error.

On the other hand, liposomes 3 complex showed fourfold release of the inner content with the increase of temperature: 0.007 min⁻¹ at 25°C and 0.029 min⁻¹ at 37°C. The maximal release was 0.08 and 0.21 for the complexes at 25°C and 37°C, correspondingly (Figure 9, curve 4).

The release experiments (Figure 9) confirmed the possibility to govern the pH-induced release from the liposomes by their modification with the linear polycation and the release dependence on the lipid trigger molar fraction. In the case of liposomes 2, the amount of lipid trigger (5% molar) was insufficient for the effective disturbance of the lipid

Figure 7 Electrophoretic mobility (curves 1 and 3) and effective diameter (curves 2 and 4) of polylysine complexes with anionic liposomes 2 (A) and liposomes 3 (B) (cf Methods section) as functions of the total concentration of polylysine. Clip = 0.625 mg/mL (C_anionic = 0.24 mmol/L). Tris buffer 1 mmol/L (pH 7.4), T=25°C.

Abbreviations: pLys, α-polylysine hydrobromide; EPM, electrophoretic mobility; D_eff, effective hydrodynamic diameter.

Figure 8 (A) Relative fluorescence intensity of labeled liposomes 3 (cf Methods section) vs polylysine concentration, pH=7.4 (1) and pH=5.5 (2). (B) Changes in the relative fluorescence intensity of labeled liposomes 3 complex with polylysine ([–]/[+]=1.3) after NaCl addition. Complex formed at pH=7.4 (1), at pH=5.5 (2), and complex formed at pH=7.4 and titrated with NaCl at pH=5.5 (3). Clip =1 mg/mL (C_anionic =0.39 mmol/L), T=25°C.
membrane after pH change. Thus, we chose the system with fliposomes 3 for the next experiment. Herein, we want to address the following question: Can the above-mentioned approach be applicable for the fliposome system loaded with a real drug? The pH-induced release of anticancer drug DXR from fliposomes 3 was further investigated for that purpose.

Tunable pH-induced release – doxorubicin release (fliposomes 3)

DXR was incorporated into the fliposomes by remote loading driven by ammonium sulfate gradient (see the details in Methods section). Acidic pH is not required for liposomal preparation by this method, which is critical for the formation of liposomes containing the pH-sensitive agent in the membrane. The difference in ammonium concentration in the inner and outer volume of liposomes induces a transmembrane pH-gradient with the intraliposomal pH=5.5. We have shown (Figures 6 and 9) that the decrease in pH value to 5.5 can induce defect formation in the fliposomal membrane and this can cause a decrease in ammonium gradient during the formation of fliposomes. Thus, we have used fliposomes 3, as the individual fliposomes in this case showed no release at pH=5.5 (Figure 9A, curve 1), while the modification of those fliposomes with polylysine led to the release of the encapsulated salt (Figure 9, curve 2). DXR accumulated in the liposomal inner volume due to the formation of a gel-like precipitate of DXR-sulfate salt inside the liposomes. The precipitation of DXR does not reduce its bioavailability.

The pH-induced release was followed by the increase of fluorescence intensity due to the increase of DXR concentration in the inner solution (Figure 10). This experiment was conducted in PBS with 0.15 M NaCl at 37°C. The decrease of pH value to 5.5 induced the immediate release of anticancer drug both from individual fliposomes and fliposomes in complex. Most part of the drug was released within the first 5 minutes after pH change. The maximal release was 0.08 and 0.47 of the loaded drug for individual fliposomes 3 and fliposomes 3 in complex, correspondingly. These data correlated very well with the release of

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**Figure 9** Time-dependent pH-induced release for individual fliposomes 2 (1) and fliposomes 2 in complex with polylysine with [+]=[−]=0.5 (2); individual fliposomes 3 (3) and fliposomes 3 in complex with polylysine with [+]=[−]=0.5 (4) at 25°C (A) and 37°C (B). C<sub>lip</sub>=1 mg/mL C<sub>ammonium</sub>=0.39 mmol/L; acetate buffer, 1 mmol/L, pH=5.5.

**Figure 10** Time-dependent pH-induced release of doxorubicin from individual fliposomes 3 (1) and fliposomes 3 in complex with polylysine (2). C<sub>lip</sub>=1 mg/mL (C<sub>ammonium</sub>=0.39 mmol/L); acetate buffer, 1 mmol/L, pH=5.5, T=37°C.
salt from the same fliposomes (Figure 9B), although the mechanism of the release of salt and DXR is different. The pH-induced lipid trigger flip is responsible for the salt release through the pores in the liposomal membrane. DXR release is more complicated since it is affected by several factors: phase state of the lipid bilayer, permeability of the liposomal membrane, and the solubility of the drug encapsulated into the liposomes. The major mechanism of DXR release is diffusion of the deprotonated drug through the liposomal membrane via dissolution–diffusion mechanism; thus, an increase in membrane permeability results in an increase in release rate. The decrease of outer pH value to 5.5 induces the flip of lipid trigger and formation of the defects that increases the permeability of the membrane and facilitates the leakage of DXR from the fliposomes. As the defects are also permeable for the buffer components, it leads to the disruption of the buffer transmembrane gradient and deprotonation of DXR inside the liposomes.

Conclusion
We have investigated the influence of the linear biocompatible polylysine on the pH-induced release from the anionic fliposomes at two different temperatures (25°C and 37°C). As the adsorption of polylysine on the anionic fliposomes did not induce flip-flop of anionic lipids, the liposomal membrane was not disturbed and polylysine did not cause the release at neutral pH. The pH responsivity of the fliposomes was achieved by embedding of the lipid trigger into the liposomal membrane. The amount of lipid trigger affects the ability of fliposomes to release the contents after the pH change. The salt release from the fliposomes with lipid trigger molar fraction 0.3 was up to 0.26 at 37°C, while from the fliposomes with TR molar fraction 0.05 and 0.1 showed only a slight salt release (up to 0.03) at the same temperature. We demonstrated that the modification of fliposomes with linear polylysine can both accelerate (fliposomes 1) and “turn on” (fliposomes 3) the release of encapsulated compound after decreasing the pH. The model salt release experiments can predict the release of the encapsulated drug. Moreover, the obtained data can help to predict the specificity of the pH-induced release from the fliposomes in physiological media in the presence of blood proteins.

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Disclosure
The authors report no conflicts of interest in this work.

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