Using additional pressure control lines when connecting a continuous renal replacement therapy device to an extracorporeal membrane oxygenation circuit

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Abstract

Background: The introduction of a continuous renal replacement therapy (CRRT) device into the extracorporeal membrane oxygenation (ECMO) circuit is widely used. However, excessive pressure transmitted to the CRRT device is a major disadvantage. We investigated the effects of using additional pressure control lines on the pressure and the lifespan of the CRRT circuit connected to the ECMO.

Methods: This is an observational study using prospectively collected data from consecutive patients receiving CRRT connected into the ECMO circuit at a university-affiliated, tertiary hospital from January 2013 to December 2016. The CRRT circuit was connected into the ECMO circuit through the Luer Lock connection without an additional pressure control line in 16 patients (9%, no line group), an additional pressure control line on the inlet line in 36 patients (23%, single line group), and additional pressure control lines on both the inlet and outlet lines in 118 patients (77%, double line group). The outcome measures of interest were compared among the three groups.

Results: The median access pressure was higher in the no line group compared to the groups. However, median filter pressure, effluent pressure, and return pressure were higher in the double line group compared to the other groups. There were no significant differences in platelets, lactate dehydrogenase, and plasma hemoglobin among the 3 groups over the time period studied. Median lifespan of the CRRT circuits in the double line group was 45.0 (29.0–63.7) hours, which was higher compared to 21.8 (11.6–31.8) hours in the no line group and 23.0 (15.0–34.6) hours in the single line group, respectively. In addition, in-hospital mortality was lower in the double line group (48.3%) compared to the no line group (68.8%) and the single line group (75.0%).

Conclusions: Additional tubing can be considered a simple and safe method for pressure control and lengthening circuit survival when connecting the CRRT device to the ECMO circuit.

Keywords: Renal replacement therapy, Extracorporeal membrane oxygenation, Critical care, Acute kidney injury

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Background
Acute kidney injury (AKI) and fluid overload frequently develop in critically ill patients receiving extracorporeal membrane oxygenation (ECMO) support for severe cardiopulmonary insufficiency [1, 2] and are associated with poor prognosis [3, 4]. Continuous renal replacement therapy (CRRT) provides an efficient and potentially beneficial method of renal replacement and fluid management in patients receiving ECMO support [5, 6], however, combining these two separate extracorporeal circuits remains a challenge [5–7]. Conceptually, the idea of connecting the CRRT device to the ECMO circuit is a convenient way to operate the CRRT device without additional catheter insertion, but in practice, there are several technical concerns. One of the major disadvantages of incorporating the CRRT device into the ECMO circuit is excessive positive or negative pressure transmitted to the CRRT device, resulting in unpredictable consequences [8]. Although several studies suggested measures to handle this problem [8–11], no standardized method exists.

Pressure is the product of flow and resistance, and both are influenced by various factors, such as diameter and length of the conduit and fluid viscosity [12]. Therefore, introducing additional tubing between the CRRT device and the ECMO circuit when connecting these two extracorporeal systems is a simple method to reduce blood flow between the systems and, ultimately, control the excessive pressures [11]. However, there is limited information available on the effects of this method on CRRT in the clinical setting. The objective of this study was to investigate the effects of using additional pressure control lines on the pressure and the lifespan of the CRRT circuit in adult patients receiving CRRT connected to the ECMO circuit.

Methods
Study population
We reviewed consecutive adult patients treated with ECMO for circulatory or respiratory failure at Samsung Medical Center in Seoul, South Korea between January 2013 and December 2016. A total of 455 ECMO runs in 431 patients were identified during the study period. After excluding 261 patients who did not receive CRRT during ECMO support, we investigated 170 patients in whom the CRRT device was connected into the ECMO circuit (Fig. 1). The institutional review board of Samsung Medical Center approved this study and waived the requirement for informed consent because of the observational nature of the study.

ECMO equipment
Patients with circulatory or respiratory failure refractory to conventional therapy were considered as candidates for ECMO [3]. Mode and cannulation were determined according to the patient’s condition. A 20–28-Fr multistage venous cannula was used for drainage via the common femoral vein, and a 14–18-Fr or 20–24-Fr short cannula was used for venous return via the internal jugular or the common femoral vein, respectively. In venoarterial mode, a 14–24-Fr cannula was inserted into the femoral artery. The Prolonged Life Support System (Quadrox PLS, Maquet Inc., Rastatt, Germany) and the Capiox Emergency Bypass System (Capiox EBS; Terumo, Inc., Tokyo, Japan), which includes a centrifugal pump and heparin-coated polypropylene hollow fiber membrane oxygenator, were available in our hospital. Pump blood flow and sweep gas flow rates were adjusted to maintain optimal tissue perfusion and gas exchange. Anticoagulation was achieved by intravenous heparin
titrated to an activated clotting time between 180 and 220 s or activated partial thromboplastin time between 55 and 75 s. Argatroban was used as an alternative anticoagulant when heparin-induced thrombocytopenia was suspected or confirmed. Anticoagulant was stopped in the presence of active bleeding at the discretion of the attending physician. Fluids or drugs were administered directly to the patient’s venous line, and the ECMO circuit was not used for this purpose. Pre-pump venous drainage, pre-membrane pressures, and post-membrane pressures were not routinely measured.

**Connection of CRRT lines to ECMO circuit**
Before 2013, our institution performed CRRT through a separate vascular access independent of the ECMO circuit. Since 2013, however, we have directly connected the CRRT device into the ECMO circuit in the following manner: inlet (access) line of the CRRT device to post-pump ECMO circuit and outlet (return) line of the CRRT device to pre-pump ECMO circuit through the Luer Lock connection [8]. Prior to July 2013, we did not utilize an additional line in the connection of the CRRT device and the ECMO circuit (Fig. 2a). In July of 2013, we connected the inlet line of the CRRT circuit to the port of the post-pump ECMO circuit with an additional pressure control line (inner diameter 1.5 mm, length 30 cm; Hyupsung Medical Co., Gyeonggi-do, South Korea) to manage excessive pressure on the inlet line of the CRRT device transmitted from the positive pressure part of the ECMO circuit. The outlet line was connected to the port of the ECMO circuit at the pre-pump ECMO circuit without an additional pressure control line (Fig. 2b). After November 2013, we modified the connection of the outlet line to the port of the ECMO circuit at the pre-centrifugal pump, adding an additional pressure control line similar to the connection of the inlet line of the CRRT circuit to the ECMO circuit (Fig. 2c).

**Management of CRRT**
CRRT was performed using the Prismaflex system (Baxter International, Deerfield, IL, USA) and the Prismaflex ST100 circuit. All Prismaflex systems installed with software, FLEX version 8.1. The priming volume was 152 mL. All patients were dialyzed in CVVHDF (continuous veno-venous hemodiafiltration) modality. Commercially prepared bicarbonate-buffered replacement fluid was used as dialysate and replacement fluid. The ultrafiltration rate and dialysate flow rate were adjusted according to clinical requirements in the range of 1000–2000 mL/h (25–35 mL/kg/h). Replacement fluid was delivered in predilution mode. Standard anticoagulation in our hospital is intravenous heparinization. If a patient had already received systemic anticoagulation with intravenous heparin or argatroban, anticoagulation was not performed for CRRT. If a patient could not maintain systemic anticoagulation due to bleeding, regional anticoagulation with nafamostat (Futhan®, SK chemicals, Seoul, Korea) for CRRT [13] or discontinuation of anticoagulant was considered. Filter was changed after 72 h of use following manufacturer’s recommendations when CRRT is needed for more than 72 h, or as needed due to filter clotting.

Under supervision of the nephrologist, nurse practitioners and registered nurses were trained to manage the CRRT system and the clinical needs of the patients on CRRT. Bedside nurses were responsible for running, maintaining, and troubleshooting the CRRT system. Orders for CRRT were the responsibility of the nephrologist. The intensive care unit (ICU) physicians were permitted to write orders to adjust fluid removal rates in collaboration with the nephrologist.

**Data collection and clinical outcomes**
The following data were collected prospectively from 2013 onward as part of the clinical care for all patients on CRRT in our ICU: patient demographics, comorbidities,
acute physiology and chronic health evaluation (APACHE) II score on ICU admission, clinical reason for CRRT initiation, setting and parameters of CRRT, and anticoagulation method. The data were recorded on the first day of CRRT initiation. The inlet and outlet pressures of the CRRT circuit displayed on the CRRT device were recorded prospectively. We used pressure values after initiating CRRT for the first time or changing to a new filter to minimize the influence of the filter condition as much as possible in assessing the effect of ECMO on CRRT depending on the connection method. To address the primary research question of whether additional pressure control lines influence CRRT circuit pressures, we measured the pressure on the added lines as well. Laboratory data were obtained before CRRT initiation, 24 h after CRRT initiation, and 48 h after CRRT initiation. Additional patient data, including illness severity, reasons for ECMO, mode of ECMO, cannulations, and anticoagulation, were extracted from the ECMO registry. ECMO circuit pressures were not monitored during the study period.

The primary outcome in this study was the lifespan of the CRRT circuit. Secondary outcomes were pressures in the CRRT circuit and changes in laboratory findings indicating hemolysis and thrombus formation before and 24 h after CRRT initiation. Clinical outcomes such as rate of weaning from ECMO, duration of ECMO support, adverse events during ECMO, and in-hospital mortality were also identified through medical record review.

Statistical analysis
Data are presented as median and interquartile range (IQR) for continuous variables and as numbers (percentages) for categorical variables. The baseline characteristics and outcome measures of interest were then compared among the three study groups: no additional pressure control line, single line group, and double line group. Data were compared using the Kruskal–Wallis test for continuous variables and the chi-square or Fisher’s exact test for categorical variables. Multiple comparisons were performed to compare each group using Wilcoxon rank sum tests, and Bonferroni correction was used to determine whether multiple comparisons were significant. To adjust for potential confounding factors in the association between additional pressure control line and lifespan of the CRRT circuit, Cox’s proportional hazards analysis was used. Data are presented as adjusted hazard ratios (HRs) with 95% confidence intervals (CI). Kaplan–Meier estimation was used to determine the lifespan curves of the CRRT circuits by different methods, which were then compared using the log-rank test. For all analyses, a two-tailed test with a $P$-value < 0.05 was considered statistically significant. Statistical analyses were performed using STATA version 14.0 (Stata Corp, College Station, TX, USA).

Results
Baseline characteristics
The baseline characteristics of the 170 patients who received CRRT during ECMO support are shown in Table 1. Median age was 56 (45–65) years and 103 (67%) patients were male. The median APACHE II on ICU admission was 23 (15–30). Cardiogenic shock (34%) and cardiopulmonary arrest (34%) were the most common reason for ECMO support, followed by respiratory failure (23%) and septic shock (7%). The majority mode of cannulation for ECMO was venoarterial (75%). The median size of drainage and return cannulas were 22 (21–24) Fr and 16 (15–17) Fr, respectively.

Initiation of CRRT
During the study period, CRRT was initiated in a median of 1 (0–2) day after ECMO initiation. The CRRT circuit was connected to the ECMO circuit through the Luer Lock connection without additional pressure control lines in 16 (9%) patients (no line group). An additional pressure control line was connected on the inlet line of the CRRT circuit in 36 (23%) patients (single line group) and on both the inlet and outlet lines in 118 (77%) patients (double line group).

Comparisons of patient characteristics, CRRT parameters, and laboratory findings at the time of CRRT initiation among the three groups are presented in Table 2. The no line group had a higher incidence of metabolic acidosis as a reason for CRRT initiation compared to the double line group. In addition, the no line group was prescribed higher blood flow, dialysate flow and replacement fluid flow of CRRT compared to the double line group. However, there was no difference in prescribed CRRT doses and fluid balances among the three groups. Regional nafamostat was more commonly used for anticoagulation in the no line group compared to the single line group and the double line group, respectively. However, the majority of patients received systemic heparin for anticoagulation, which was not significantly different among three groups. There was no significant difference in laboratory findings at the time of CRRT initiation, except for serum HCO$_3^-$, which was lower in the single line group compared to the double line group.

Parameters of CRRT and clinical outcomes according to connection method
The pressure values of the CRRT circuits are presented in Table 3. The median access pressure was higher in the no line group (163 mmHg) compared to the single line group (37 mmHg) and the double line group (2 mmHg). However, median filter pressure, effluent pressure, and return
pressure were higher in the double line group compared to the no line group and the single line group. There were no significant differences in the laboratory values of platelets, lactate dehydrogenase, and plasma hemoglobin from CRRT initiation to 24 and 48 h after treatment initiation among the 3 groups (Table 3).

The median lifespan of the CRRT circuits in the double line group was 45.0 (29.0–63.7) hours, which was higher compared to 21.8 (11.6–31.8) hours in the no line group (P < 0.001) and 23.0 (15.0–34.6) hours in the single line group (P < 0.001), respectively. When filter survival rates were compared 72 h after CRRT initiation, the Kaplan-Meier survival estimates showed a significantly higher filter survival rate in the double line group compared to the no line group and the single line group (log rank test, P < 0.001) (Fig. 3).

Clinical outcomes of patients who received CRRT during ECMO support are shown in Table 4. There was no difference in ECMO related complications among the three groups. Although the median duration of ECMO support was longer, however, in-hospital mortality was lower in the double line group compared to the single line group.

The results of univariable and multivariable analyses with the proportional hazards regression model for probability of circuit change within 72 h are presented in Table 5. After adjusting for potential confounding factors, the double line group was still significantly associated with lower change of the CRRT circuit (adjusted HR 0.39, 95% CI 0.25–0.60). Other factors independently associated with circuit change within 72 h were type of ECMO, anticoagulation, filter pressure, and return pressure in the CRRT circuits.

**Discussion**

In the present study, we investigated the efficacy and safety of using additional pressure control lines to control the pressure on CRRT by connecting the CRRT device to the ECMO circuit. Our findings suggest that the high positive or negative pressure values of the CRRT were attenuated and the lifespan of the CRRT circuit was significantly increased after using the additional lines on both the inlet and outlet lines of the CRRT device connected into the ECMO circuit. Furthermore, the use of multiple lines was not associated with an increase in hemolysis-related complications.

Patients receiving ECMO often suffer acute kidney injury for a number of reasons, such as severe cardiopulmonary insufficiency requiring ECMO support, use of vasoactive drugs or mechanical ventilation before ECMO, and ECMO-associated systemic inflammation [5]. Although CRRT is a common practice in patients receiving ECMO, determining the vascular access to connect the CRRT device, another extracorporeal circuit,

### Table 1 Patient characteristics upon initiation of extracorporeal membrane oxygenation

| Characteristics                                      | No. of patients (%) or median (IQR) |
|------------------------------------------------------|------------------------------------|
| Age, years                                           | 57 (47–65)                         |
| Male                                                 | 115 (67.6)                         |
| Body mass index, kg/m²                                | 24.7 (22.3–27.6)                   |
| Comorbidities                                         |                                    |
| Cardiovascular disease                                | 33 (19.4)                          |
| Chronic renal failure                                 | 22 (12.9)                          |
| Asthma/COPD                                          | 7 (4.1)                            |
| Liver cirrhosis                                      | 8 (4.7)                            |
| Malignancy                                           | 36 (21.2)                          |
| Severity of illness on ICU admission                 |                                    |
| APACHE II                                            | 23 (15–30)                         |
| Reasons for ECMO support                             |                                    |
| Cardiogenic shock                                    | 57 (33.5)                          |
| Cardiopulmonary arrest                               | 57 (33.5)                          |
| Respiratory failure                                  | 37 (21.8)                          |
| Septic shock                                         | 11 (6.5)                           |
| Weaning failure of CPB                               | 4 (2.4)                            |
| Hypovolemic shock                                    | 3 (1.8)                            |
| Other                                                | 1 (0.6)                            |
| Cannulation for ECMO                                 |                                    |
| Venoarterial                                         | 127 (74.7)                         |
| Venovenous                                           | 40 (23.5)                          |
| Mixed                                                | 3 (1.8)                            |
| Cannula size                                         |                                    |
| Drainage cannula, Fr                                 | 22 (21–24)                         |
| Return cannula, Fr                                   | 16 (15–17)                         |
| ECMO flow, L/min                                     | 3.7 (3.1–4.2)                      |
| Anticoagulation                                      |                                    |
| Unfractionated heparin                               | 107 (62.9)                         |
| Argatroban                                           | 4 (2.4)                            |
| None                                                 | 61 (35.7)                          |
| Laboratory findings on ECMO initiation               |                                    |
| Blood urea nitrogen, mg/dL                           | 34.5 (23.2–55.7)                   |
| Creatinine, mg/dL                                    | 1.83 (1.26–2.79)                   |
| Bicarbonate, mmol/L                                  | 17.6 (13.0–21.8)                   |
| Potassium, mmol/L                                    | 4.2 (3.8–4.9)                      |
| Platelets, 10⁹/μL                                    | 89 (53–142)                        |
| Lactate dehydrogenase (n = 152), IU/L                | 1551 (903–2853)                    |
| Plasma hemoglobin (n = 50), mg/dL                    | 18.5 (13.0–32.0)                   |

*APACHE II acute physiology and chronic health evaluation II, COPD chronic obstructive pulmonary disease, CPB cardiopulmonary bypass, ECMO extracorporeal membrane oxygenation, ICU intensive care unit, IQR interquartile range*
is still a challenging problem. One of three possible connection methods is used to perform CRRT in patients on ECMO [7]. One method is to use a vascular access independent from the ECMO circuit as in patients not receiving ECMO. It is possible to control the ultrafiltration via CRRT independent of the ECMO hemodynamics. However, there is an inherent risk of complications associated with catheter insertion; the use of an anticoagulant during ECMO in particular increases the risk of bleeding complications [14]. Another method is to connect the hemodiafilter into the ECMO circuit without an in-line CRRT device and control the ultrafiltration using an intravenous infusion pump. Although this is relatively simple and can avoid complications associated with an additional catheter insertion, several studies reported errors in controlling ultrafiltration via an infusion pump. In addition, since the pressure of the hemodiafilter circuit cannot be monitored, there is a limit to the early detection of mechanical complications of the circuit [6, 9, 15].

Therefore, the introduction of a CRRT device into the ECMO circuit is widely used in many centers [16]. This method enables precise control of ultrafiltration through the CRRT device and monitoring of pressure parameters on the CRRT circuit. However, one of the major disadvantages of incorporating the CRRT device into the ECMO circuit is the interference of blood flow in the CRRT and ECMO circuits [6].

| Characteristics | No line group (n = 16) | Single line group (n = 36) | Double line group (n = 118) | P value |
|-----------------|------------------------|---------------------------|-----------------------------|--------|
| Age, years      | 59 (48–65)             | 54 (36–62)                | 58 (48–65)                  | 0.241  |
| Male            | 12 (75.0)              | 24 (66.7)                 | 79 (66.9)                   | 0.804  |
| Body mass index, kg/m² | 23 (21–26)             | 24.5 (22.5–27.4)          | 25.0 (22.1–28.0)            | 0.291  |
| ECMO flow, L/min | 3.5 (2.6–4.1)          | 3.5 (3.0–4.2)             | 3.8 (3.2–4.3)               | 0.192  |
| Indication for CRRT |                       |                           |                             |        |
| Acute kidney injury | 2 (12.5)              | 8 (22.2)                  | 31 (26.3)                   | 0.461  |
| Volume overload  | 6 (37.5)               | 15 (41.7)                 | 59 (50.0)                   | 0.492  |
| Metabolic acidosis | 11 (68.8)              | 20 (55.6)                 | 35 (29.7)                   | 0.001† |
| Prescription of initial CRRT |           |                           |                             |        |
| Blood flow, mL/min | 150 (150–150)         | 150 (150–150)            | 150 (150–150)               | 0.013† |
| CRRT dose, mL/kg/hr | 40 (31–46)            | 36 (27–44)               | 32 (27–44)                  | 0.062  |
| Dialysate flow, mL/hr | 1250 (1000–1500)      | 1000 (1000–1500)         | 1000 (1000–1500)            | 0.033  |
| Replacement fluid flow, mL/hr | 1250 (1000–1500)       | 1000 (1000–1500)         | 1000 (1000–1500)            | 0.041  |
| Prescribed fluid balance, mL/hr | 0 (–40–0)              | 0 (–40–0)                | –20 (–43–0)                 | 0.189  |
| Anticoagulation for CRRT |               |                           |                             |        |
| Systemic heparin | 9 (56.3)              | 22 (61.1)                 | 76 (64.4)                   | 0.792  |
| Regional heparin | 0 (0.0)               | 0 (0.0)                   | 0 (0.0)                     | –      |
| Regional nafamostat | 5 (31.3)              | 4 (11.1)                  | 3 (2.5)                     | <0.001†|
| Systemic argatroban | 0 (0.0)               | 0 (0.0)                   | 4 (3.4)                     | 0.406  |
| None            | 4 (25.0)              | 12 (33.3)                 | 37 (31.4)                   | 0.833  |
| Laboratory findings on CRRT initiation |             |                           |                             |        |
| Blood urea nitrogen, mg/dL | 28.2 (18.3–41.8)      | 29.7 (18.7–55.9)         | 38.9 (24.2–59.3)            | 0.105  |
| Creatinine, mg/dL | 1.76 (1.42–2.27)      | 1.78 (1.23–2.95)         | 1.93 (1.26–3.07)            | 0.587  |
| Bicarbonate, mmol/L | 18.1 (14.2–19.6)      | 14.7 (11–18.1)           | 18.9 (13.8–22)              | 0.034‡ |
| Potassium, mmol/L | 4.0 (3.5–5.2)         | 4.1 (3.9–4.8)            | 4.3 (3.8–4.9)               | 0.675  |
| Platelets, 10³/µL | 88 (68–128)           | 102 (49–152)             | 87 (53–140)                 | 0.945  |
| Lactate dehydrogenase (n = 152), IU/L | 2256 (1531–4350) | 1451 (799–4442)         | 1498 (945–2512)             | 0.276  |
| Plasma hemoglobin (n = 50), mg/dL | 48.9 (42.7–NA) | 136 (9.8–22.6)          | 185 (13.3–31.3)             | 0.090  |

CRRT continuous renal replacement therapy, CVVH continuous venovenous hemofiltration, CVVHDF continuous venovenous hemodiafiltration

Superscripts †, ‡ indicate significant differences (p < 0.05) between the no line group and the double line group, and the single line group and the double line group, respectively
ECMO circuit causes excessive positive or negative pressure above the physiological range to the CRRT device, which eventually leads to an interruption of CRRT [6, 8, 9]. There are various suggestions for improvement, such as changing the connection site of the ECMO circuit, adjusting the alarm value of the CRRT software, and using a clamp to control the pressures [8–11], but all are associated with potentially unpredictable consequences [10].

Drawing upon the physical law that reducing the lumen of the conduit increases the resistance and reduces blood flow and pressure, we applied an additional line in which the lumen was narrower than those of the inlet and outlet lines of the CRRT circuit between the CRRT device and the ECMO circuit to modify the excessive pressures. This is supported by Suga et al. who investigated the method of connecting an additional pressure-resistant tube (diameter 1.5 mm) to control the pressure transmitted from the ECMO circuit in an in vitro study [11]. Although the inlet and outlet pressures remained within the safety range for all conditions of ECMO and CRRT flow in the in vitro study, the method was validated in only two clinical cases.

### Table 3 Comparisons of parameters of CRRT among the study groups after connecting additional pressure control lines

| CRRT parameters | No line group (n = 16) | Single line group (n = 36) | Double line group (n = 118) | P value |
|-----------------|-----------------------|---------------------------|---------------------------|---------|
| **Pressures on CRRT circuit** | | | | |
| Access pressure, mmHg | 163 (117–185) | –37 (–65–57) | 2 (–42–52) | < 0.001*† |
| Filter pressure, mmHg | –17 (–67–24) | –25 (–49–25) | 119 (73–167) | < 0.001†‡ |
| Effluent pressure, mmHg | –101 (–138 – –24) | –104 (–139 – –59) | 19 (–17–60) | < 0.001†‡ |
| Return pressure, mmHg | –81 (–108 – –41) | –71 (–108 – –44) | 68 (29–107) | < 0.001†‡ |
| Transmembrane pressure, mmHg | 57 (36–93) | 53 (25–78) | 58 (46–69) | 0.746 |
| Pressure drop, mmHg | 36 (28–42) | 32 (20–42) | 25 (16–33) | 0.003† |
| **Change in laboratory findings** | | | | |
| ΔPLT between H0 and H24, mg/dL | –27 (–68 – –3) | –1 (–51–27) | –15 (–41–7) | 0.289 |
| ΔPLT between H0 and H48, mg/dL | –41 (–101–4) | 4 (–76–13) | –16 (–45–12) | 0.427 |
| ΔLD between H0 and H24, IU/L | 482 (–650–3405) | 384 (–109–1580) | –3 (–237–248) | 0.069 |
| ΔLD between H0 and H48, IU/L | 482 (–53–2648) | 22 (–2237–1237) | 20 (–496–263) | 0.354 |
| ΔpHb between H0 and H24 (n = 17), mg/dL | NA | 23.5 (9 – NA) | –5 (–20–2) | 0.037 |
| ΔpHb between H0 and H48 (n = 23), mg/dL | NA | 12.5 (12 – NA) | 3 (–5–8) | 0.100 |
| Lifespan of CRRT circuit, hours | 21.8 (11.6–31.8) | 23.0 (15.0–34.6) | 45.0 (29.0–63.7) | < 0.001†‡ |

**CRRT** continuous renal replacement therapy, **LD** lactate dehydrogenase, **pHb** plasma hemoglobin, **PLT** platelets

Superscripts *, †, ‡ indicate significant differences (p < 0.05) between the no line group and the single line group, the no line group and the double line group, and the single line group and the double line group, respectively.

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**Fig. 3** Kaplan–Meier estimate of the lifespan of the continuous renal replacement therapy circuit.
In our study with a large number of clinical cases, we found that the excessive positive or negative pressure above the physiological range transmitted from the ECMO circuit to the CRRT circuit could be controlled to remain within the safety range using additional lines on both the inlet and outlet lines of the CRRT device connected into the ECMO circuit without complications. In addition, the filter pressure was confirmed to be within the safety range when connected to the ECMO circuit. Owing to the stability of the CRRT system, a longer lifespan of the CRRT circuit was achieved without complications, compared to those reported in previous studies [10, 17, 18].

Table 4 Comparisons of clinical outcomes among the study groups after connecting additional pressure control lines

| Clinical outcomes                  | No line group (n = 16) | Single line group (n = 36) | Double line group (n = 118) | P value |
|-----------------------------------|------------------------|---------------------------|----------------------------|---------|
| Duration of ECMO support, hours   | 80 (53–467)            | 93 (32–189)               | 184 (93–501)                | 0.003‡  |
| Successful weaning from ECMO      | 6 (37.5)               | 17 (47.2)                 | 72 (61.0)                  | 0.103   |
| ECMO complication                  |                        |                           |                            |         |
| Gastrointestinal bleeding         | 2 (12.5)               | 1 (2.9)                   | 16 (13.8)                  | 0.201   |
| ECMO site bleeding                | 2 (12.5)               | 8 (22.9)                  | 15 (12.9)                  | 0.339   |
| Cerebral infarction               | 2 (12.5)               | 4 (11.4)                  | 3 (2.6)                    | 0.053   |
| Sepsis                            | 3 (18.8)               | 5 (14.3)                  | 10 (8.6)                   | 0.356   |
| In-hospital mortality             | 11 (68.8)              | 27 (75.0)                 | 57 (48.3)                  | 0.010 psychiatrist[C]  |

ECMO extracorporeal membrane oxygenation

Table 5 Univariable and multivariable analyses with Cox’s proportional hazards model for probability of circuit change within 72 h

| Additional pressure control line | Univariable HR 95% CI | P value | Multivariable aHR 95% CI | P value |
|---------------------------------|------------------------|---------|--------------------------|---------|
|                                 |                        |         |                         |         |
| No line                         | –                      | –       | –                       | –       |
| Single line                     | 0.69 0.53–0.91         | 0.008   | 0.74 0.46–1.19           | 0.216   |
| Double line                     | 0.29 0.23–0.37         | < 0.001 | 0.39 0.25–0.60           | < 0.001 |
| ECMO type                       |                        |         |                         |         |
| Venoarterial                    | –                      | –       | –                       | –       |
| Venovenous                      | 2.05 1.72–2.44         | < 0.001 | 1.33 1.06–1.67           | 0.013   |
| Mixed                           | 0.41 0.15–1.11         | 0.079   | 0.45 0.16–1.27           | 0.132   |
| Size of drainage cannula, Fr    | 1.07 1.03–1.11         | 0.001   | 1.01 0.97–1.06           | 0.549   |
| Size of return cannula, Fr      | 1.09 1.04–1.13         | < 0.001 | 1.06 1.01–1.13           | 0.028   |
| Use of unfractionated heparin    | 0.56 0.47–0.67         | < 0.001 | 0.64 0.52–0.78           | < 0.001 |
| Metabolic acidosis              | 1.42 1.17–1.72         | < 0.001 | 1.17 0.95–1.43           | 0.147   |
| Access pressure, mmHg           | 1.001 1.000–1.002      | 0.027   | 1.000 0.998–1.002        | 0.957   |
| Filter pressure, mmHg           | 0.995 0.994–0.996      | < 0.001 | 1.006 1.002–1.010        | 0.007   |
| Effluent pressure, mmHg         | 0.995 0.994–0.996      | < 0.001 | 1.000 0.998–1.002        | 0.956   |
| Return pressure, mmHg           | 0.994 0.993–0.995      | < 0.001 | 0.994 0.990–0.998        | 0.005   |

CI confidence interval, ECMO extracorporeal membrane oxygenation; HR hazard ratio
compared with the ECMO flow [11]. Similar to our model, Santiago et al. [9] suggested that connecting the inlet and outlet lines of the CRRT device after the centrifugal pump would be safe and effective. However, the connection of the outlet line into the positive pressure part of the ECMO circuit can trigger excessive pressure on the outlet line, generating alarms inside the CRRT machine. Our results indicate that this could be managed by additional tubing on the connection.

This study provides information on the use of additional tubing in connecting a CRRT device to an ECMO circuit, but there are several limitations that should be acknowledged. First, given the retrospective and observational nature of our study, there is a potential risk of selection bias and confounding variables. Treatment group size was unbalanced and allocation was non-randomized, resulting in differences in baseline characteristics between groups. And laboratory tests such as plasma hemoglobin were obtained in only a few patients. However, the data were prospectively collected from all patients receiving CRRT during ECMO support. Second, our study demonstrated the effects of using additional tubing on the pressure values and circuit lifetime of a CRRT device. It is difficult to explain the effect on the ECMO circuit because the pressures on the ECMO circuit were not measure. Third, about three-quarters of the patients included in our study had circulatory failure that required venoarterial extracorporeal life support, and this hemodynamic status influenced physicians to describe a relatively low CRRT blood flow rates. Along with this, anticoagulation strategy was different between group without and with additional pressure control lines. These factors could affect the overall circuit lifespan. However, we think that the absolute blood flow rates and differences of anticoagulation strategy had little effect on comparison of CRRT circuit lifespan depending on use of additional pressure line because the blood flow rates and anticoagulation were similar between group with additional pressure control line at inlet line only and group with additional pressure control line at both inlet and outlet lines, a major interest of our study. Last, we did not compare our connection method with additional tubing to other configurations. A standardized connection method has not been established, and our interest was in using additional tubing to effectively control pressures of the CRRT device. Further studies should evaluate the effects of additional tubing with various connections of the CRRT device into the ECMO circuit.

Conclusions
The present study suggests that the use of additional tubing can be considered a simple and safe method for pressure control and improvement of filter survival when connecting a CRRT device into an ECMO circuit in adult patients. However, further prospective studies should be conducted to investigate the configuration of the two extracorporeal systems and the effect on ECMO hemodynamics.

Abbreviations
AKI: Acute kidney injury; APACHE: Acute physiology and chronic health evaluation; CRRT: Continuous renal replacement therapy; CVVHDF: Continuous veno-venous hemodiafiltration; ECMO: Extracorporeal membrane oxygenation; ICU: Intensive care unit; IQR: Interquartile range

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Availability of data and materials
All data generated or analyzed during the present study are included in this published article.

Authors’ contributions
Research conception and study design: SJN, HJC, KJ; data acquisition: SJN, HJC; data analysis/interpretation: SJN, HJC, CRC, YHC, HRJ, GYS, KJ; statistical analysis: SJN, HJC, KJ; supervision or mentorship: KJ. All authors have read and approved the final manuscript.

Ethics approval and consent to participate
The institutional review board of the Samsung Medical Center approved this study and waived the requirement for informed consent because of the observational nature of the study.

Consent for publication
Not applicable.

Competing interests
The authors declare that they have no competing interests.

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