Lower extremity kinematic analysis in male athletes with unilateral anterior cruciate reconstruction in a jump-landing task and its association with return to sport criteria

Sadegh Norouzi1, Fateme Esfandiarpour1,2*, Sina Mehdizadeh3, Nasim Kiani Yousefzadeh1 and Mohamad Parnianpour4

Abstract

Background: Return to sport (RTS) criteria are widely being used to identify anterior cruciate ligament reconstructed (ACLR) athletes ready to return to sportive activity and reduce risk of ACL re-injury. However, studies show a high rate of ACL re-injury in athletes who passed RTS criteria. This indicates that the current RTS criteria might not be sufficient to determine return to sport time in ACLR athletes. Previous studies have reported a close association between altered lower limb kinematics and ACL re-injury. However, it is not clear how lower extremity kinematics differs between ACLR athletes who passed the RTS-criteria and who failed. This study compared lower extremity kinematics in a jump-landing task between ACLR athletes who passed the RTS criteria (Limb symmetry in hop tests, quadriceps strength and questionnaires) to those who failed and to the healthy individuals.

Methods: Participants were 27 male football players with unilateral ACLR including 14 who passed -RTS criteria and 13 failed, and 15 healthy football players. A 3D motion capture system recorded participants' lower extremity motion while performing 10 trials of a bilateral jump-landing task. Hip, knee and ankle angular motion were examined at initial contact. Two-way mixed analysis of variances (2 limbs × 3 groups) and Bonferroni post-hoc tests were performed to compare the joint angles between the limbs and groups.

Results: Lower hip abduction angle was found in the failed (involved limb 4.1° ± 4.2) and passed RTS (involved limb 6.8° ± 3.3) groups compared to the healthy group (non-dominant limb 10.7° ± 3.7). Ankle inversion in the failed RTS (0.4° ± 4.9) group was significantly lower than both passed RTS (4.8° ± 4.8, p = 0.05) and healthy (8.2° ± 8.1, p < 0.001) groups. There were no significant differences between the groups in knee kinematics.

Conclusions: Our findings indicate reduced hip abduction during initial contact phase of landing in athletes returned to sport. Reduced hip abduction during the complex multiplanar movement of jump-landing is a risk factor for ACL re-injury. Current RTS criteria may not be sufficient to identify ACLR athletes at high risk of re-injury. The kinematic analysis in conjunction with current RTS criteria can provide additional insight into the return to sport decision making.

Keywords: Anterior cruciate ligament, Landing kinematics, Return to sport, Clinical decision-making, soccer
**Background**

Anterior Cruciate Ligament reconstruction (ACLR) followed by rehabilitation is the ‘gold standard’ protocol following an ACL injury in athletes, with the ultimate goal to return to sport [1]. Return to sport (RTS) criteria has been developed to return athletes as fast as possible to their pre-injury performance level while reducing the risk of re-injury [2–4]. RTS is based on a decision-making process including multidimensional aspects [3]. Assessing the level of functional/neuromuscular restoration by using quadriceps strength test, single-legged hop tests, and self-report questionnaires [5] is the most important aspect of the RTS process.

Despite ongoing progress in surgery and rehabilitation protocols for ACLR, recent studies show that athletes are still at a high risk of ACL re-injury post-surgery [6, 7]. It has been reported that ACL re-injury rates range from 22 to 30% in both affected and contralateral knees and up to 10% in the ipsilateral knee within a 10-year follow-up period [7]. Bien et al. (2015) suggested that the high rate of ACL re-injury in athletes could indicate flaws in the return to sport criteria [2].

The underlying causes for ACL re-injury are multifactorial and not limited to muscle strength deficit and/or functional performance as considered in RTS [6]. Previous studies consistently reported an association between lower limb kinematics especially during multiplanar and complicated activities such as landing and ACL injury/re-injury [8–10]. Moreover, the results of prospective studies by Paterno et al. (2010), and in Leppänen et al. (2017) indicated that altered landing biomechanics is an important predictive factor of ACL injury/re-injury [8, 11]. Based on Kyritsis et al. (2016) study, current RTS criteria have an acceptable predictability to identify athletes at risk of re-injury [12]. Despite this, the rate of ACL re-injury remain high [2]. This might highlights importance of kinematic analysis together with current RTS to provide more detailed information to return to sport decision making. It is not clear whether a good performance in muscle symmetry and functional test as measured in RTS is also indicative of a safe lower extremity kinematic pattern.

Despite the close association between altered lower limb kinematics and ACL re-injury [8, 13], there is still a lack of knowledge regarding kinematic differences between athletes who passed the RTS-criteria and who failed. A recent study by Chang et al. (2019) investigating knee kinematic differences in female athletes who pass or fail RTS criteria pass and healthy females found no significant difference between in knee kinematics between the groups [14]. However, there is still no related report regarding kinematic differences in male athletes and in the hip and ankle kinematic as contributing factors to ACL re-injury in ACLR athlete [15]. Investigation of lower extremity landing kinematic differences in these two groups of athletes and to their healthy counterparts could reveal the underlying cause of ACL re-injury in passed-RTS athletes and will serve as the first step towards a more accurate decision making on return to sport readiness of ACLR athletes.

The present study thus aimed to analyze hip, knee and ankle 3D joint kinematics during the initial contact phase of landing task, i.e. minimum vertical velocity of ankle segment [16], in three groups of athletes: passed-RTS, failed-RTS, and healthy individuals. We hypothesize that the lower limb landing kinematics is different between the three groups and this difference is not revealed in the RTS criteria.

**Methods**

**Participants**

Twenty-seven athletes with ACLR (23.8 ± 3.3 years) and 15 healthy athletes with no history of any lower extremity injury (24.6 ± 3.1 years) participated in this cross-sectional study. Out of 27 participants with unilateral ACLR, 14 passed the RTS criteria (passed-RTS group), while 13 did not (failed-RTS group). Table 1 presents the characteristics of the participants of the three groups. All Participants were male football players, recruited from the local sport physiotherapy clinics and football clubs over a period of 6 months. Inclusion criteria were: age 18 to 40 years, unilateral ACL reconstruction at least 6 months before the study beginning [5, 17], ability to perform regular jumping and pivoting activities (≥50 h per year) before the injury [18]. The exclusion criteria were a meniscal tear of greater than grade I [19], osteochondral defect, a complete tear of other knee ligaments, a history of other lower extremity joint surgery and neuromuscular disorders in the hip, knee, ankle and lower back that limits the ability of athletes to perform sports activities. Participants in the control group had no history of lower limb and back injury or surgeries. The ACLR participants completed a progressive rehabilitation treatment supervised by licensed sports physiotherapists, and had full knee ROM, knee joint effusion of grade trace or zero based on the stroke test [20] and ability to perform the single-hop test without pain. A sport physiotherapist screened participant for the inclusion/exclusion criteria. All participants read and signed an informed consent approved by the university ethics committee (ethics approval number: IR.AJUMS.REC.1396.579).

**Study procedure**

Participants underwent RTS and kinematic assessments in two separate testing sessions. In the first session, their demographic data including age, weight, height, and Tegner score (before the injury and 6 months after ACLR) [21] were recorded. They were also asked to fill
the Knee Outcome Survey–Activities of Daily Living Scale (KOS-ADL) and the Global Knee Rating Scale questionnaires for each limb separately and without any specific cutoff [22]. An experienced sports physiotherapist performed the RTS testing. Participants were allocated to the failed and passed RTS group based on the outcomes of four commonly accepted RTS criteria including maximal isometric quadriceps strength, four functional single-legged hop tests (single, triple, crossed and 6-m-time-to-hop), the KOS-ADL and the Global Knee Rating Scale questionnaires. These particular tests are considered important to estimate the functional/neuromuscular status of athlete who want return to their pre-injury level of activities [3]. Quadriceps strength test was performed using a hand held dynamometer according to the standard belt-stabilized method [23]. For the hop tests for distance, athletes stood on one leg with their toes behind the starting line, hopped forward as far as possible and landed on the same leg. For the single and triple hop tests, athletes performed a single hop, and three consecutive hops, respectively. For the crossed hop test, they performed three consecutive hops while crossing the midline with each hop. The distance of hop was recorded for each test in centimeters (cm). For the 6-m hop test, they hopped on one leg as quickly as possible over a distance of 6 m. The tests were performed in random order and for both legs to calculate the limb symmetry index (LSI) (involved/uninvolved) [24]. To pass the RTS criteria, each participant had to gain a minimum LSI of 0.90 on all RTS criteria. All RTS tests were performed at least 6 months after ACL reconstruction [5].

Jump-landing task
All participants performed a light intensity pedaling on a stationary bicycle for 5 min to warm-up before participating in the jump-landing test. For the jump-landing task, the participants jumped from a 30 cm box and landed at a distance of 50% of body height away from the box (as the landing area) followed by a maximal vertical jump [9]. Each participant performed 2 practice trials, followed by 10 actual test trials. A trial was considered successful if the individual jumped bilaterally from the box, landed in the landing area. Participants could rest at least 1 min between the consecutive trials. Participants wore a pair of standard athletic shoes that has previously been adjusted to place the reflective markers.

Kinematic data analysis
Ten successful jump-landing tests for each limb were used for further analyses using Visual3D software (C-Motion Inc., Kingston, Canada). Data was low pass filtered with a cutoff frequency of 6 Hz followed by identifying the initial contact using the lower leg segment’s vertical velocity. We concentrated on the initial contact of the landing task because previous studies demonstrated that ACL injury/re-injury mostly occurs at the initial contact of landing [8, 26, 27]. That is, the minimum vertical velocity of the lateral malleolus marker [16] was used as the initial contact moment. Moreover, manual inspection was used to verify correct identification and adjustment when required. Cardan angles were used to define the joint angles. The sequence of rotation was x-y-z, based on the recommendations of the International Society of Biomechanics [28]. Hip, knee and ankle kinematics in the three anatomical planes of motion were examined at initial contact, and the average of the 10 landing trials was used for statistical analysis. The positive sign assigned to the hip and knee flexion,

| Table 1 Participant characteristics, mean (SD) |
|--------------------------------------------|
|                                       | Failed-RTS | Passed-RTS | Healthy | F     | Sig. |
| Age (year)                               | 24.3 (3.8) | 23.1 (2.5) | 24.6 (3.1) | 0.747 | 0.412 |
| Height (cm)                              | 176.3 (6.3) | 179.5 (6.2) | 174.6 (4.6) | 2.501 | 0.094 |
| Weight (kg)                              | 72.1 (9.1) | 73.9 (8.1) | 69.1 (5.2) | 1.405 | 0.257 |
| Time since Injury (months)               | 7.5 (1.5) | 7.7 (1.3) | –       | 0.135 | 0.734 |
| Tegner Score before injury               | 8.1 (1.1) | 8.6 (0.7) | 8.4 (1.1) | 1.427 | 0.252 |
| Tegner Score after injury                | 6.8 (0.75) | 8.1 (1.1) | –       | 11.982 | 0.002 |

Abbreviations: RTS Return to Sport, F F ratio, Sig Significance set at p < 0.05
adduction, and internal rotation, ankle dorsiflexion, and ankle eversion.

**Statistical analysis**

Statistical analysis was completed using IBM SPSS Statistics Version 25.0 (SPSS, Inc., Chicago, IL), and statistical significance was set at $p < 0.05$. Normality of distribution of kinematic data was checked using Shapiro–Wilk normality tests. The limb symmetry indices for the functional, quadriceps strength and questionnaires tests (Table 2), and demographic characteristics (Table 1) were compared between the three groups using one-way analysis of variances (ANOVAs). The kinematic variables were compared between the limbs (involved/uninvolved) and the groups (passed-RTS, failed-RTS and healthy) using nine separate mixed ANOVAs. Post-hoc tests with Bonferroni adjustment were performed to locate the source of significance.

**Results**

There was no significant difference between the failed-RTS and the passed-RTS groups for the time passed from ACL reconstruction ($p = 0.73$). In addition, there were no significant differences between the groups for age, height, weight and the Tegner score before the injury ($p > 0.05$; Table 1).

The failed-RTS group had lower symmetry index for the single hop ($p = 0.036$), triple hop ($p = 0.024$) and crossed hop ($p = 0.017$) tests compared to the healthy group. However, there were no significant differences between the failed- and passed-RTS groups and the passed-RTS and the healthy group for the hop tests ($p > 0.05$) regarding the limb symmetry index. Moreover, there was no significant difference between the three groups in terms of the quadriceps strength symmetry index ($p > 0.05$). However, participants in the failed-RTS group had lower Tegner score (6 months after ACLR) compared to the passed-RTS group ($F = 11.1, p = 0.002$). The failed-RTS group also obtained lower scores for the global rating knee scale and KOS-ADL compared to the passed-RTS group (Table 2). Table 3 present raw values of each RTS tests.

**Kinematics**

No significant limb-by-group interactions were found for the hip, knee, and ankle 3D kinematics ($p > 0.05$). The main effect of group was significant for hip abduction/adduction ($F = 10.541, p < 0.001$), hip rotation ($F = 5.081, p = 0.011$) and ankle eversion/inversion ($F = 11.384, p < 0.001$). The post-hoc comparisons revealed lower hip abduction angle in both failed (involved limb $10.6^\circ \pm 4.2, p < 0.001$) and passed RTS (involved limb $11.6^\circ \pm 3.1, p = 0.006$) groups compared to the healthy group (non-dominant limb $16.6^\circ \pm 3.7$). However, hip abduction was not different between the failed- and passed-RTS groups ($p > 0.05$). With regard to hip transverse plane kinematics, post-hoc test found lower hip external rotation in the failed-RTS group (involved limb $12.7^\circ \pm 6.1$) compared to the healthy group (non-dominant limb $15.7^\circ \pm 8.3, p = 0.01$), but no significant differences between the failed- and passed-RTS groups ($p = 0.152$), and also between the passed-RTS and healthy groups ($p = 0.923$).

There were no significant differences between the groups in knee kinematics ($p > 0.05$). Ankle inversion in the failed-RTS (involved limb $10.2^\circ \pm 5.1$) was significantly lower than both the passed-RTS (involved limb $12.1^\circ \pm 4.8, p = 0.05$) and the healthy (non-dominant limb $22.1^\circ \pm 8.2, p < 0.001$) groups. Finally, there was no significant difference between the passed-RTS and the healthy groups for ankle inversion/eversion ($p = 0.117$).

### Table 2 Return to sport criteria, between groups comparison

|                      | Healthy mean (SD) | Passed-RTS mean (SD) | Failed-RTS mean (SD) | F     | Sig. |
|----------------------|-------------------|----------------------|----------------------|-------|------|
| Quadriceps LSI       | 100.8 (8.3)       | 103.3 (17.6)         | 93.1 (8.1)           | 3.169 | 0.053|
| Single hop LSI       | 101.6 (5.2)       | 98.7 (4.9)           | 95.0 (7.7)           | 3.467 | 0.041|
| Triple hop LSI       | 102.7 (4.6)       | 100.5 (2.9)          | 96.1 (9.4)           | 4.049 | 0.025|
| Crossed hop LSI      | 101.1 (4.1)       | 100.1 (0.3)          | 93.5 (10.2)          | 4.980 | 0.012|
| 6-m hop LSI          | 103.1 (10.6)      | 101 (7.5)            | 100.7 (15.1)         | 0.188 | 0.930|
| Global rating scale  | –                 | 93.3 (4.1)           | 82.5 (10.3)          | 12.589| 0.001|
| KOS-ADL              | –                 | 95.1 (4.5)           | 76.0 (9.3)           | 45.082| < 0.001|

**Abbreviations:** RTS Return to Sport, LSI Limb symmetry index, KOS-ADL Knee Outcome Survey Activities of Daily Living Scale, $F$ F ration, $\text{Sig}$ Significance set at $p < 0.05$; a indicates significant differences between failed and healthy; symbol b indicates significant differences between failed and passed
The main effect of limb was only significant for hip abduction/adduction ($F = 9.383$, $p = 0.006$). The involved limb of failed-RTS had lower hip abduction compared to the non-involved limb (mean difference = 5.45° ± 6). The passed-RTS group and the healthy athletes had relatively similar hip abduction/adduction (Table 4 and Fig. 1).

**Discussion**

The aim of this study was to compare lower limb kinematics of 3 groups of athletes including two ACL reconstructed (passed- and failed-RTS criteria) and a healthy group. In support of our hypothesis, we found significant differences in the hip and ankle kinematics between the passed-RTS, failed-RTS and healthy athletes. Our findings revealed reduced hip abduction in athletes who passed RTS compared to the healthy athletes despite an acceptable functional status in RTS. However, there was no significant difference in hip abduction angle between the passed- and failed-RTS groups although having different RTS criteria. This implies that RTS criteria cannot identify improper lower extremity kinematics in a landing task which could signify the cause of re-injury in passed-RTS ACLR athletes. Our results also demonstrated a significant difference between the failed- and passed RTS groups in ankle inversion/eversion angle.

Quadriceps strength of failed, pass and healthy athletes was similar for both involved and non-involved limb (dominant and non-dominant for healthy athletes). For all hop tests, healthy athletes obtained greater score compared to the failed and passed groups. Moreover, pattern of raw data and LSI (Tables 2 and 3) of each criterion was similar. This shows that not only are those in the Passed-RTS group more symmetrical than the failed group that they also scored better on every outcome (farther jump distances, higher strength, better self-reported outcomes). In our study, number of athletes who failed two self-report questionnaires were higher that those who failed the hop tests. This may indicate the role of psychological factors for readiness to return to sport [29, 30]. Based on Table 2, a maximum of only 3 people failed the RTS criteria for any hop test. While group analyses showed that the people in the Failed-RTS group were significantly different than controls for the single, triple and crossed hops. Similar finding was also reported by Ebert et al. (2018) [31]. This might show that the hop tests have low sensitivity for discriminate ACLR athlete who may be at risk of re-injury.

**Table 3** Return to sport criteria, raw data

|                      | Failed mean (SD) | Passed mean (SD) | Healthy mean (SD) |
|----------------------|------------------|------------------|-------------------|
|                      | involved | Non-involved | involved | Non-involved | Non-dominant | dominant |
| Quadriceps strength (N) | 64.3 (14.2) | 65.1 (13.5) | 66.4 (7.8) | 68.1 (11.9) | 59.7 (12.3) | 61 (13) |
| Single hop (cm)       | 167.4 (25) | 174.3 (23.58) | 189.1 (24.7) | 189.5 (22.37) | 213.6 (11.56) | 211 (18) |
| Triple hop (cm)       | 485.5 (67.9) | 507 (81.8) | 578.4 (89.1) | 573.5 (87.6) | 603.3 (82.5) | 591.3 (77.4) |
| Crossed hop (cm)      | 417 (77.8) | 441.6 (83.13) | 454.3 (88.2) | 451.6 (80) | 544.3 (63.3) | 538 (63.9) |
| 6-m hop(s)            | 2.4 (0.5) | 2.4 (0.6) | 2.1 (0.4) | 2.2 (0.5) | 1.5 (0.3) | 1.6 (0.3) |
| Global rating scale   | 75 (9.8) | 91.2 (10.3) | 90.5 (10.1) | 96.1 (10.4) | – | – |
| KOS-ADL               | 68.3 (9.3) | 89.1 (9.8) | 91 (8.8) | 97 (10.2) | – | – |

**Abbreviations:** N Newton, cm centimeter, s second, SD standard deviation

**Table 4** The mean (standard deviation) of lower extremity angles (°) at the initial contact of landing

|                  | Hip | Knee | Ankle |
|------------------|-----|------|-------|
|                  | Flex | Add  | Flex | Add | Int Rot | DorsiFlex | Eversion | Int Rot |
| Healthy          |      |      |      |     |         |           |          |        |
| Non-dominant     | 37.8 (8.3) | −16.6 (3.7) | −15.7 (8.3) | 68.4 (6.2) | −4.5 (6.4) | −11.5 (8.4) | 11.1 (4) | −22.1 (8.2) | −9.1 (7.5) |
| Dominant         | 37.6 (9.1) | −17.8 (4.4) | −19.3 (6.4) | 64.4 (7.1) | −4.5 (9.1) | −22.6 (8.3) | 8.4 (5.1) | −16.4 (5.2) | −6.8 (6.2) |
| Passed-RTS       |      |      |      |     |         |           |          |        |
| Involved         | 44.3 (7.1) | −11.6 (3.1) | −15.1 (6.1) | 63.2 (7.6) | −0.8 (4.1) | −13.5 (7.1) | 12.8 (3.3) | −12.1 (4.8) | −9.5 (6.2) |
| Non-involved     | 43.2 (6.7) | −14.6 (3.1) | −19.1 (5.3) | 66.1 (7.5) | −4.5 (5.1) | −15.5 (5.1) | 11.1 (3.8) | −11.7 (4.1) | −2.8 (3.3) |
| Failed-RTS       |      |      |      |     |         |           |          |        |
| Involved         | 34.5 (9.8) | −10.6 (4.2) | −12.7 (6.1) | 62.4 (6.3) | −18.1 (8.3) | −17.1 (9.1) | 12.8 (3.8) | −102 (5.1) | −7.2 (7.3) |
| Non-involved     | 40.4 (10.6) | −17.6 (4.3) | −17.5 (6.8) | 67.1 (6.4) | −8.5 (6.3) | −15.6 (7.1) | 13.1 (3.4) | −7.2 (4.8) | −13.2 (7.1) |

**Abbreviations:** Flx flexion, Ext extension, Abd abduction, Add adduction, Int/Ext Rot Internal/External Rotation

For the ankle joint: Flx: Dorsi Flexion, Ext: Plantar Flexion, Abd: Eversion, Add: Inversion
Comparison of the passed-RTS and healthy group

In the passed-RTS group, despite appropriate improvement in the muscle strength and functional performance (LSI ≥ 90%), lower hip abduction angle was found compared to the healthy group. This result is consistent with previous studies that reported a tendency toward hip abduction during walking and landing in individuals with ACLR who returned to play [25, 32]. Research suggests an association between ACL injury and excessive hip abduction and internal rotation during multiplanar movement, e.g., landing [8, 33]. Thus, reduced hip abduction and external rotation seen in ACLR athletes who passed RTS criteria may indicate that current strength and function-based RTS criteria is not sufficient to identify athletes at risk of ACL re-injury and highlights the need for lower extremity kinematic analysis together with current RTS criteria. Altered hip kinematics in athletes who passed RTS may also suggest the need for more attention to the strengthening of the hip and core stabilizers, and neuromuscular training following ACLR as positive effects of hip strengthening and neuromuscular training on changing frontal plane hip motion reported in previous studies [34–36].

Comparison of the failed-RTS and healthy group

This is in agreement with the results of a recent study by Xergia et al. (2015) who found no significant correlation between functional asymmetry assessed by LSI for the hop test and lower extremity kinematics during landing [37]. However, similar hip and knee kinematics of failed- and passed-RTS groups in our study is contrary to the finding of Di Stasi et al. (2013) who found different hip and knee kinematics in the passed- and failed-RTS groups during treadmill walking [5]. This controversy may be due to the differences in the task evaluated, as it has been shown that the kinematics of gait and landing tasks are not associated [38].

Similar lower extremity kinematics in failed- and passed-RTS groups indicates that passed RTS athletes still have biomechanical risk factors for ACL re-injury similar to the failed group despite passing the return to sport criteria. Therefore, kinematic analysis together with current RTS may provide more detailed information for increased safety to return to sport decision making.

In our study, participant in the failed-RTS group landed with less ankle inversion when compared with the passed-RTS group. Because of linked motion between lower extremity joints during close kinetic chain tasks such as landing, changes in the ankle frontal plane motion may impact hip and knee joint kinematics [39, 40] and may increase the risk of ACLR injury/re-injury [41]. Previous studies reported that Change in ankle motion during landing may contribute to Transverse plane hip and frontal plane knee positioning when contacting the ground, which are known to increase the risk of lower extremity injury [42, 43].

Comparison of the failed-RTS and healthy group

Hip abduction (mean diff = 4.5°), hip external rotation (mean diff = 5.6°), and ankle inversion (mean diff = 7.8°)
were significantly lower in the failed-RTS group compared to the healthy group. Previous studies also reported significant differences between the ACLR and healthy groups in peak hip flexion [17, 24], hip abduction/adduction [25] and frontal plane knee motion [44]. Decreased hip abduction, external rotation and ankle inversion may increase tendency toward dynamic valgus phenomena in the initial phase of landing which is an important risk factor to ACL re-injury [8]. Adam et al. (2018), in a meta-analysis, showed that individuals with ACLR land with increased hip abduction in the involved limb compared to the intact limb [25].

Limb comparison
We found lower hip abduction angle in the ACL reconstructed limb compared to the intact limb in the failed-RTS athletes. This may explain the higher rate of re-injury in the ACL reconstructed limb in individuals with a history of unilateral ACLR. That is, increased hip abduction, which can lead to a valgus knee position, is known as an important risk factor that can predict the risk of ACL re-injury [8]. Adam et al. (2018), in a meta-analysis, also showed that individuals with ACLR land with increased hip abduction in the involved limb compared to the intact limb [25].

Study limitation
One limitation of our study is that we did not evaluate hip muscles strength. This was because the focus of this study was to investigate the association between RTS criteria and lower extremity kinematics. Several studies, however, reported a relationship between hip strength and lower extremity kinematics during challenging activities such as landing [45, 46], step descent [47] and hopping [48]. Future studies should consider hip muscle strength while comparing lower extremity kinematics in the ACLR knee. Moreover, this study included only male participants which limit generalizability of our outcomes to females with ACLR. This was mainly due to the low rate of female ACLR athletes in our available population. Also considering kinetic data in conjunct with kinematics in the future studies can improve our knowledge about landing biomechanics as a suggested task to evaluate of athlete readiness to return to sport after ACLR and its relationship with current RTS criteria. Finally, Current RTS testing is performed under pre-planned/anticipated circumstances. There is a plethora of studies investigating the effects of unplanned/unanticipated jump landings/cuttngs on lower limb biomechanics [49–51]. As team sport athletes interacting in a variable and unforeseen environment, such tests may better mimic the realistic affordances (increase ecological validity).

Conclusion
Our finding indicated reduced hip abduction during landing in athletes who released to return to sport despite nearly normal functional and muscle strength scores. Reduced hip abduction during a complex multi-planar movement such as jump-landing is a risk factor for ACL re-injury. Most of current RTS criteria are mainly based on muscle strength and functional evaluation without consideration of alteration in lower extremity kinematics. Findings of this study support our hypothesis that current RTS criteria may not be sufficient to differentiate athletes at high risk of ACL re-injury. Kinematic analysis in conjunction with current RTS criteria can provide additional insight into return to sports decision making.

Abbreviations
ACL: Anterior cruciate ligament; ACLR: Anterior cruciate ligament reconstruction; GRS: Global rating scale; KOS-ADL: Knee outcome survey scale-activity daily living; LSI: Limb symmetry index; RTS: Return to sport

Acknowledgements
This is a part of Ph.D thesis of Dr. Sadegh Norouzi (former Ph.D candidate) at Ahvaz Jundishapur University of medical sciences.

Authors’ contributions
SN developed the research idea, carried out the experiment, analyzed and interpreted the data supervised by his mentors, and drafted the manuscript. This article is the product of his Ph.D dissertation. FE had a substantial contribution to the development of the study, data analysis, data interpretation, and the manuscript evaluation. SM led and supervised kinematics analysis. He also had a significant contribution to the evaluation and revision of the manuscript. NKY helped with data collection and data entry. MP reviewed and commented on the research proposal and final draft of the manuscript. All authors read and approved the final manuscript.

Funding
This study was partly funded by Ahvaz Jundishapur University of medical sciences (grant number: Phd-9615). The funding bodies had no role in the design of the study and collection, analysis, and interpretation of data or in writing the manuscript.

Availability of data and materials
The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

Ethics approval and consent to participate
This study was approved by the ethics committee (No: IR.AJUMS.REC.1396.579) of Ahvaz Jundishapur University of Medical Sciences. All participants read and signed an informed consent approved by the ethics committee.

Consent for publication
Not Applicable.

Competing interests
The authors declare that they have no competing interests.
References

1. Paschos NK, Howell SM. Anterior cruciate ligament reconstruction: principles of treatment. EORT Open Rev. 2016;1(11):388–408. https://doi.org/10.1032/2058-5241.160032.

2. Bien DP, Dubuque TJ. Considerations for late stage acl rehabilitation and return to sport to limit re-injury risk and maximize athletic performance. Int J Sports Phys Ther. 2015;10(2):256–71.

3. Creighton DW, Shier I, Shultz P, Meeuwisse WH, Matheson GO. Return-to-play in sport: a decision-based model. Clin J Sport Med. 2010;20(3):79–85. https://doi.org/10.1097/01.jsm.0000381831e1cf6.

4. Grindem H, Snyder-Mackler L, Mokones H, Engebretsen L, Risberg MA. Simple decision rules can reduce reinjury risk by 84% after ACL reconstruction: the Delaware-Oslo ACL cohort study. Br J Sports Med. 2016;50(10):1097–104. https://doi.org/10.1136/bjsports-2015-095251.

5. Paschos NK, Howell SM. Anterior cruciate ligament reconstruction: differences and similarities. Am J Sports Med. 2005;33(9):1337–45. https://doi.org/10.1177/0363546504271415.

6. Paterno MV, Schmitt LC, Ford KR, Rauh MJ, Myer GD, Huang B, et al. Simple decision rules can reduce reinjury risk by 84% after ACL reconstruction: a systematic review and meta-analysis. J Athl Train. 2018;53(2):144–59. https://doi.org/10.1177/0196653517745487.

7. Pinczewski LA, Lyman J, Salmon LJ, Russell VJ, Roe J, Linklater J. A 10-year comparison of anterior cruciate ligament reconstructions with hamstring tendon and patellar tendon autograft: a controlled, prospective trial. Am J Sports Med. 2007;35(4):564–74. https://doi.org/10.1177/0363546506069204.

8. Paterno MV, Schmitt LC, Ford KR, Rauh MJ, Myer GD, Huang B, et al. Biomechanical measures during landing and postural stability predict second anterior cruciate ligament injury after anterior cruciate ligament reconstruction and return to sport. Am J Sports Med. 2010;38(8):1968–78. https://doi.org/10.1177/0363546510365705.

9. Paterno MV, Schmitt LC, Ford KR, Rauh MJ, Myer GD, Huang B, et al. Risk factors for anterior cruciate ligament injury: a review of the literature - part 1: neuromuscular and anatomic risk. Sports Health. 2012;4(1):69–78. https://doi.org/10.1177/1941738111428281.

10. Paterno MV, Schmitt LC, Ford KR, Rauh MJ, Myer GD, Huang B, et al. Incidence and predictors of second anterior cruciate ligament injury after primary reconstruction and return to sport. J Athl Train. 2015;50(10):1097–1105. https://doi.org/10.4085/1062-6050-50.10.07.

11. Paterno MV, Kiefer AW, Bonnette S, Riley MA, Schmitt LC, Ford KR, et al. Prospectively identified deficits in sagittal plane hip-ankle coordination in female athletes who sustain a second anterior cruciate ligament injury after anterior cruciate ligament reconstruction and return to sport. Clin Biomech (Bristol, Avon). 2015;30(10):1094–101. https://doi.org/10.1016/j.clinbiomech.2015.08.019.

12. Paterno MV, Kiefer AW, Bonnette S, Riley MA, Schmitt LC, Ford KR, et al. Psychological factors associated with anterior cruciate ligament reconstruction recovery. Orthop J Sports Med. 2014;2(3):2325967114538314. https://doi.org/10.1177/2325967114538314.

13. Paterno MV, Kiefer AW, Bonnette S, Riley MA, Schmitt LC, Ford KR, et al. Psychological factors associated with anterior cruciate ligament reconstruction recovery. Orthop J Sports Med. 2014;2(3):2325967114538314. https://doi.org/10.1177/2325967114538314.

14. Paterno MV, Kiefer AW, Bonnette S, Riley MA, Schmitt LC, Ford KR, et al. Prospectively identified deficits in sagittal plane hip-ankle coordination in female athletes who sustain a second anterior cruciate ligament injury after anterior cruciate ligament reconstruction and return to sport. Clin Biomech (Bristol, Avon). 2015;30(10):1094–101. https://doi.org/10.1016/j.clinbiomech.2015.08.019.

15. Tengeman E, Grip H, Stensdottir A, Hager CK. Anterior cruciate ligament injury about 20 years post-treatment: a kinematic analysis of one-leg hop. Scand J Med Sci Sports. 2015;25(6):818–27. https://doi.org/10.1111/sms.12434.

16. Butler RJ, Dai B, Huffman N, Garrett WE, Queen RM. Lower extremity movement differences persist after anterior cruciate ligament reconstruction and when returning to sports. Clin J Sport Med. 2016;26(5):411–6. https://doi.org/10.1097/JSM.0000000000000279.

17. White K, Logerstedt D, Snyder-Mackler L. Gait Asymmetries Persist 1 Year After Anterior Cruciate Ligament Reconstruction. Orthop J Sports Med. 2013;1(2). https://doi.org/10.1177/2325967113496697.

18. Roe J, Pinczewski LA, Russell VJ, Salmon LJ, Kawamura T, Chew M. A 7-year follow-up of patellar tendon and hamstring tendon grafts for arthroscopic anterior cruciate ligament reconstruction: differences and similarities. Am J Sports Med. 2005;33(9):1337–45. https://doi.org/10.1177/0363546504271415.

19. Sturgill LP, Snyder-Mackler L, Manal TJ, Aix MJ. Intererater reliability of a clinical scale to assess knee joint effusion. J Orthop Sports Phys Ther. 2009;39(12):845–9. https://doi.org/10.2519/jospt.2009.3143.

20. Mostafaei N, Neghaban H, Shaterzadeh Yazdi M, Goharyep S, Mehravar M, Piraye H. Responsiveness of a Persian version of knee injury and osteoarthritis outcome score and Tegner activity scale in athletes with anterior cruciate ligament reconstruction following physiotherapy treatment. Physiother Theo Pract. 2018;1–8. https://doi.org/10.1080/09593985.2018.1548672.

21. Collins NJ, Milia D, Felson DT, Crossey KM, Roos EM. Measures of knee function: International Knee Documentation Committee (IKDC) Subjective Knee Evaluation Form, Knee Injury and Osteoarthritis Outcome Score (KOOS), Knee Injury and Osteoarthritis Outcome Score Physical Function Short Form (KOOS-PS), Knee Outcome Survey Activities of Daily Living Scale (KOS-ADL), Lysholm Knee Scoring Scale, Oxford Knee Score (OKS), Western Ontario and McMaster Universities Osteoarthritis Index (WOMAC), Activity Rating Scale (ARS), and Tegner Activity Score (TAS). Arthritis Care Res (Hoboken). 2011;63 Suppl 1: S120–7. https://doi.org/10.1002/acr.20632.

22. Hansen EM, McCartney CN, Sweeney RS, Palmenio MR, Grindstaff TL. Hand-held dynamometer positioning impacts discomfort during quadriiceps strength testing: a validity and reliability study. Int J Sports Phys Ther. 2015;10(1):62–8.

23. Xingia SA, Pappas E, Zampeli F, Georgiou S, Georgouls AD. Asymmetries in functional hop tests, lower extremity kinematics, and isokinetic strength persist 6 to 9 months following anterior cruciate ligament reconstruction. J Orthop Sports Phys Ther. 2013;43(3):154–62. https://doi.org/10.2519/jospt.2013.39367.

24. Lepley AS, Kuenze CM. Hip and knee kinematics and kinetics during landing tasks after anterior cruciate ligament reconstructions: a systematic review and meta-analysis. J Athl Train. 2018;53(2):144–59. https://doi.org/10.4085/1062-6050-334-16.

25. Meyer CAG, Gette P, Mouton C, Sel R, Theisen D. Side-to-side asymmetries in landing mechanics from a drop vertical jump test are not related to asymmetries in knee joint laxity following anterior cruciate ligament reconstruction. Knee Surg Sports Traumatol Arthrosc. 2018;26(2):381–90. https://doi.org/10.1007/s00167-017-4651-2.

26. Decker MJ, Terry MR, Noonan TJ, Riviere A, Sterett WI. Landing adaptations after ACL reconstruction. Med Sci Sports Exerc. 2002;34(9):1408–13. https://doi.org/10.1249/01.MSS.0000027627.82650.1F.

27. Wu G, Siegel S, Allard P, Kirley G, Leadinnj A, Rosenthal D, et al. ISB recommendation on definitions of joint coordinate system of various joints for the reporting of human joint motion—part I: ankle, hip, and spine. Int Soc Biomech. 2002;35(4):543–8.

28. Christinie MA, Fleming BC, Machan JT, Shalvey RM. Psychological factors associated with anterior cruciate ligament reconstruction recovery. Orthop J Sports Med. 2018;6(13):2325967116638341. https://doi.org/10.1177/2325967116638341.
reconstruction: a review and meta-analysis. J Athl Train. 2017. https://doi.org/10.4085/1062-6050.52.6.06.
33. Hewett TE, Myer GD, Ford KR, Paterno MV, Quatman CE. Mechanisms, prediction, and prevention of ACL injuries: cut risk with three sharpened and validated tools. J Orthop Res. 2016;34(11):1843–53. https://doi.org/10.1002/jor.23414.

34. Willy RW, Davis IS. The effect of a hip-strengthening program on mechanics during running and during a single-leg squat. J Orthop Sports Phys Ther. 2011;41(9):625–32. https://doi.org/10.2519/jospt.2011.3470.
35. Araujo VL, Souza TR, Carvalhais V, Cruz AC, Fonseca ST. Effects of hip and trunk muscle strengthening on hip function and lower limb kinematics during step-down task. Clin Biomech (Bristol, Avon). 2017;44:28–35. https://doi.org/10.1016/j.clinbiomech.2017.02.012.
36. Wouters I, Almonroeder T, Dejarlais B, Laack A, Willson JD, Kernozek TW. Effects of a movement training program on hip and knee joint frontal plane running mechanics. Int J Sports Phys Ther. 2012;7(6):637–46.
37. Xergia SA, Pappas E, Georgoulis AD. Association of the Single-Limb hop Test with isokinetic, kinematic, and kinetic asymmetries in patients after anterior cruciate ligament reconstruction. Sports Health. 2015;7(3):217–23. https://doi.org/10.1177/1941738114529532.
38. Pfeiffer SJ, Blackburn JT, Harkey MS, Stanley LE, Frank B, et al. Peak knee biomechanics and limb symmetry following unilateral anterior cruciate ligament reconstruction: Associations of walking gait and jump-landing outcomes. Clin Biomech (Bristol, Avon). 2018;53:79–85. https://doi.org/10.1016/j.clinbiomech.2018.01.020.
39. Stanley LE, Harkey M, Luc-Harkey B, Frank BS, Pietrosimone B, Blackburn JT, et al. Ankle dorsiflexion displacement is associated with hip and knee kinematics in females following anterior cruciate ligament reconstruction. Res Sports Med. 2018;1:1–13. https://doi.org/10.1080/15438627.2018.1502180.
40. Mitchell LC, Ford KR, Minning S, Myer GD, Mangine RE, Hewett TE. Medial foot loading on ankle and knee biomechanics. N Am J Sports Phys Ther. 2008;3(1):133–40.
41. Chmielewski TL. Asymmetrical lower extremity loading after ACL reconstruction: more than meets the eye. J Orthop Sports Phys Ther. 2011;41(6):374–6. https://doi.org/10.2519/jospt.2011.0104.
42. Begalle RL, Walsh MC, McGrath ML, Boling MC, Blackburn JT, Padua DA. Ankle dorsiflexion displacement during landing is associated with initial contact kinematics but not joint displacement. J Appl Biomech. 2015;31(4):205–10. https://doi.org/10.1123/jab.2013-0233.
43. Gafner SC, Hoewel V, Punt IM, Schmid S, Armand S, Allot L. Hip-abductor fatigue influences sagittal plane ankle kinematics and shank muscle activity during a single-leg forward jump. J Electromyogr Kinesiol. 2018;43:75–81. https://doi.org/10.1016/j.elekin.2018.09.004.
44. Hart H, Culvenor G, Collins NJ, Ackland DC, Machotka Z, Cowan SM, et al. A systematic review and meta-analysis of knee kinematics and moments after anterior cruciate ligament reconstruction: Implications for post-traumatic knee osteoarthritis. Osteoarthritis Cartilage. 2015;23(2):A93–A44. https://doi.org/10.1016/j.joca.2015.02.802.
45. Suzuki H, Omori G, Uematsu D, Nishino K, Endo N. The influence of hip strength on knee kinematics during a single-legged medial drop landing among competitive collegiate basketball players. Int J Sports Phys Ther. 2015;10(5):592–601.
46. Pollard CD, Sigward SM, Powers CM. ACL injury prevention training results in modification of hip and knee mechanics during a drop-landing task. Orthop J Sports Med. 2017;5(9):232596717726267. https://doi.org/10.1177/232596717726267.
47. Olson TJ, Chebny C, Willson JD, Kernozek TW, Straker JS. Comparison of 2D and 3D kinematic changes during a single leg drop step following neuromuscular training. Phys Ther Sport. 2011;12(2):93–9. https://doi.org/10.1016/j.ptsp.2010.10.002.
48. Tate J, Suckit T, Wages J, Lyles H, Perrin B. The associations between hip strength and hip kinematics during a single leg hop in recreational athletes post ACL reconstruction compared to healthy controls. Int J Sports Phys Ther. 2017;12(3):341–51.
49. Collins JD, Almonroeder TG, Ebersole KT, O’Connor KM. The effects of fatigue and anticipation on the mechanics of the knee during cutting in female athletes. Clin Biomech (Bristol, Avon). 2016;35:62–7. https://doi.org/10.1016/j.clinbiomech.2016.04.004.
50. Meinerz CM, Malloy P, Geiser CF, Kipp K. Anticipatory effects on lower extremity Neuromechanics during a cutting task. J Athl Train. 2015;50(9):905–13. https://doi.org/10.4085/1062-6050-50.8.02.

Publisher’s Note
Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.