Computed tomography volumetry of esophageal cancer - the role of semiautomatic assessment

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Abstract

Background: The clinical and research value of Computed Tomography (CT) volumetry of esophageal cancer tumor size remains controversial. Development in CT technique and image analysis has made CT volumetry less cumbersome and it has gained renewed attention. The aim of this study was to assess esophageal tumor volume by semi-automatic measurements as compared to manual.

Methods: A total of 23 esophageal cancer patients (median age 65, range 51–71), undergoing CT in the portal-venous phase for tumor staging, were retrospectively included between 2007 and 2012. One radiology resident and one consultant radiologist measured the tumor volume by semiautomatic segmentation and manual segmentation. Reproducibility of the respective measurements was assessed by intraclass correlation coefficients (ICC) and by average deviation from mean.

Results: Mean tumor volume was 46 ml (range 5-137 ml) using manual segmentation and 42 ml (range 3-111 ml) using semiautomatic segmentation. Semiautomatic measurement provided better inter-observer agreement than traditional manual segmentation. The ICC was significantly higher for semiautomatic segmentation in comparison to manual segmentation (0.86, 0.56, \( p < 0.01 \)). The average absolute percentage difference from mean was reduced from 24 to 14% (\( p < 0.001 \)) when using semiautomatic segmentation.

Conclusions: Semiautomatic analysis outperforms manual analysis for assessment of esophageal tumor volume, improving reproducibility.

Keywords: Esophageal cancer, Computed tomography, Tumor volume, Esophageal resection
validity of this technology has to be better defined [10, 11]. Accordingly, in many referral centers, CT remains the investigation of choice, not only for staging but also for the evaluation of the effectiveness of neoadjuvant therapies [12]. In the attempt to describe the extent of the local tumor growth and also when exploring an eventual therapeutic effect of preoperative therapies, assessment of the volume of the tumor might be critical [12, 13]. Attempts have been made to apply this technique both in controlled as well as uncontrolled research protocols [13–16]. Some studies indicate that CT-determined volume of esophageal cancer may add to the assessment of neoadjuvant chemoradiotherapy effects and even add prognostic information [13, 17]. However, at present, there is no established and validated method to monitor esophageal tumor response to treatment.

The aim of the current study was therefore to compare the reproducibility of CT volumetry of esophageal tumors using traditional manual segmentation with more modern semiautomatic segmentation by consultant radiologists and radiologists under training.

### Methods

#### Patients

A subset of 23 out of 181 esophageal cancer patients (median age 65 range 51–71, 20 male, 3 female, Table 1) included in a multicenter randomized clinical trial comparing two neoadjuvant regimens during 2007 and 2012 was retrospectively analyzed [18]. The patients had newly diagnosed adenocarcinoma or squamous cell carcinoma and were planned for curative neoadjuvant treatment followed by surgical resection. Tumor histology was verified through histological typing of surgically resected tumor, or multiple endoscopic biopsies if the patient was not applicable for surgical treatment due to disease progression during neoadjuvant treatment. Patients with metastatic diseases or subject to endoscopic stent placement or other treatment prior to the CT scan were excluded. A further inclusion criterion was presence of baseline spiral CT for tumor staging from our clinic before start of neoadjuvant treatment with the presence of scans from both arterial and portal-venous phase and 0.625 mm slices.

Ethical approval for the study was granted by the regional ethical review board in Stockholm. Approval

### Table 1 Details about patients (n = 23) included for the manual segmentation and semiautomatic measurements

|   | BMI | Cancer type | TNM stage | Tumor location | Neoadjuvant therapy | Resected |
|---|-----|-------------|-----------|----------------|---------------------|----------|
| 1 | 22  | SCC         | T2N1M0    | Middle         | Chemoradiotherapy   | Yes      |
| 2 | 25  | AC          | T3N1M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |
| 3 | 25  | AC          | T2N0M0    | Distal         | Chemoradiotherapy   | No       |
| 4 | 24  | AC          | T3N1M0    | Cardia, SII    | Chemotherapy        | Yes      |
| 5 | 24  | AC          | T3N1M0    | Cardia, SII    | Chemotherapy        | Yes      |
| 6 | 22  | SCC         | T3N1M0    | Middle         | Chemotherapy        | Yes      |
| 7 | 22  | SCC         | T3N1M0    | Middle         | Chemoradiotherapy   | Yes      |
| 8 | 30  | AC          | T3N1M0    | Distal         | Chemoradiotherapy   | Yes      |
| 9 | 22  | AC          | T3N0M0    | Cardia         | Chemoradiotherapy   | No       |
| 10| 27  | SCC         | T3N1M0    | Middle         | Chemoradiotherapy   | Yes      |
| 11| 24  | AC          | T3N1M0    | Distal         | Chemotherapy        | Yes      |
| 12| 32  | SCC         | T3N1M0    | Distal         | Chemotherapy        | Yes      |
| 13| 33  | AC          | T3N1M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |
| 14| 25  | AC          | T2N0M0    | Cardia, SII    | Chemotherapy        | Yes      |
| 15| 28  | AC          | T3N1M0    | Cardia, SII    | Chemotherapy        | Yes      |
| 16| 23  | SCC         | T2N1M0    | Middle         | Chemoradiotherapy   | Yes      |
| 17| 30  | AC          | T3N0M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |
| 18| 21  | SCC         | T3N1M0    | Distal         | Chemotherapy        | No       |
| 19| 22  | SCC         | T3N1MX    | Distal         | Chemoradiotherapy   | Yes      |
| 20| 34  | AC          | T2N0M0    | Cardia, SII    | Chemotherapy        | Yes      |
| 21| 26  | AC          | T3N0M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |
| 22| 20  | AC          | T3N1M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |
| 23| 23  | AC          | T3N0M0    | Cardia, SII    | Chemoradiotherapy   | Yes      |

AC = Adenocarcinoma, SCC = Squamous cell carcinoma, SI = Siewert I, SII = Siewert II
Written informed consent was obtained.

**CT imaging acquisition parameters**

The patients underwent multi-slice CT of the thorax using multislice CT (GE Lightspeed VCT (GE Healthcare, WI, USA) or Siemens Somatom Definition Flash (Siemens AG, Erlangen, Germany). All examinations were performed at 120 kV after intravenous contrast injection of Iomeron 400 mg I/ml (Bracco, Milan Italy) in both arterial and portal phase. The tube current was automatically modulated. The dosage of contrast media was 750 mg I/kg or 1000 mg I/kg. Slice thickness was 0.625 mm. The field of view was adjusted for patient size.

**Comparison of manual and semiautomatic segmentation**

A second year resident in radiology and a consultant radiologist with 25 years of experience independently measured the tumor volume of 23 patients with esophageal cancer (middle and distal third part) by manual and semiautomatic segmentation. These patients were under baseline evaluation for curative resections for esophageal cancer after induction chemo or radio-chemo therapy.

The segmentation was performed using a dedicated workstation with GE AW 4.0 (GE Healthcare, WI, USA). Images were first reformatted to 2.5 mm and displayed as average intensity projections. CT window level settings were at the discretion of the observer. Only transaxial images were available for the observers. For the semiautomated segmentation, the first and last slice containing the primary esophageal tumor, and slices where major morphologic changes occurred, were delineated manually using a mouse controlled cursor (Fig. 1). The rest of the tumor was then first interpolated by the software and the resulting volume of interest was reviewed by the radiologist and manually adjusted by adding or removing included tumor area for each slice where disagreement with the software interpolated selection occurred. The lower and higher threshold of voxels included in the volume of interest was set to 0 and 1000 Hounsfield units respectively in order to exclude air and include all esophageal tumor tissue. The cross sectional areas of all slices were multiplied by the slice thicknesses and the total volume was calculated by summation of these volumes. The measurement of the tumors was done in both arterial and venous phase for each patient, resulting in two measurements of volume per tumor per observer.

The manual segmentation was done by the same observers at least three months after the measurement using semiautomated segmentation to reduce the effects of recall of the previous semiautomated segmentation. The tumor was manually delineated on transaxial images on every slice containing the primary esophageal tumor and tumor volume was calculated by multiplying cross sectional areas of all slices by the slice thickness and summation of the resulting volumes.

**Statistical analyses**

Data are presented as mean values (95% confidence interval of the mean, CI). Statistical significance was defined at a level of \( p < 0.05 \). Intraclass correlation coefficients (ICC) were calculated for intra and inter-observer measurements. The significance of difference in correlation was tested using a Fisher r to z calculation. To further characterize the level of observer agreement Bland-Altman plots were used to graphically visualize the level of agreement. Upper and lower limits of agreement were calculated and incorporated into the plots [19]. Observer measurement accuracy was also assessed by calculating the average absolute difference from mean for each tumor volume measurement. Comparison of tumor volume between the arterial phase and the portovenous phase was used to assess intraobserver variability of measurement.

Statistical analysis was done using R 3.4.3 (R Foundation, Vienna, Austria).

**Availability of data and material**

The datasets generated and/or analyzed during the current study are not publicly available but are available from the corresponding author on reasonable request.
Results
All tumors were detected by both observers for all included patients. Mean tumor volume when merging arterial and portovenous measurements was 46 ml (range 5-137 ml) using manual segmentation and 42 ml (range 3-111 ml) using semiautomatic segmentation, \( p = 0.30 \). No significant differences in volume were observed between adenocarcinoma and squamous cell carcinoma. All measured volumes are shown in Table 2.

Intraobserver variability of tumor assessment at CT
No statistically significant difference of mean tumor volume was observed between arterial and portovenous volume measurements for both manual and semiautomatic methods for both observers. Comparison of arterial tumor volume with portovenous volume resulted in excellent intraobserver agreement with ICC of 0.97 for both manual and semiautomatic segmentation.

Interobserver variability of tumor assessment at CT
Interobserver ICC was significantly higher for semiautomatic segmentation in comparison to manual segmentation (0.86 versus 0.56, \( p < 0.01 \)). Bland-Altman plots (Fig. 2b, d) show slightly narrower limits for semiautomatic segmentation in comparison to manual segmentation, (40.1 ml versus 56.8 ml). Significantly higher ICC was observed after semiautomatic segmentation compared to manual segmentation for measurements of adenocarcinoma (0.86 versus 0.54, \( p < 0.01 \)) but not for squamous cell carcinoma (0.88 versus 0.63, \( p = 0.052 \)). No significant differences in ICC between adenocarcinoma and squamous cell carcinoma were detected when sub analyzing the manual segmentation or semiautomatic segmentation group.

### Table 2
Measured primary esophageal tumor volume for all included patients by radiology resident and radiology consultant using manual and semiautomatic segmentation. All volumes measured in milliliters (ml)

|        | Manual |        | Semiautomatic |        |
|--------|--------|--------|---------------|--------|
|        | Resident | Venous | Consultant | Arterial | Venous | Arterial | Venous |
| 1      | 15  | 14  | 5  | 5  | 33 | 31 | 3  |
| 2      | 42  | 44  | 13 | 8  | 36 | 31 | 24 | 28 |
| 3      | 36  | 44  | 5  | 6  | 23 | 26 | 25 | 25 |
| 4      | 44  | 50  | 16 | 15 | 28 | 21 | 26 | 25 |
| 5      | 57  | 52  | 30 | 33 | 48 | 59 | 29 | 35 |
| 6      | 46  | 54  | 43 | 31 | 39 | 33 | 33 | 36 |
| 7      | 105 | 99  | 62 | 63 | 70 | 83 | 68 | 74 |
| 8      | 135 | 125 | 81 | 70 | 95 | 101 | 69 | 68 |
| 9      | 51  | 66  | 21 | 23 | 34 | 42 | 19 | 26 |
| 10     | 65  | 56  | 23 | 35 | 47 | 40 | 41 | 40 |
| 11     | 137 | 132 | 73 | 78 | 111| 110| 92 | 104|
| 12     | 73  | 81  | 58 | 59 | 59 | 62 | 59 | 54 |
| 13     | 66  | 69  | 45 | 48 | 50 | 50 | 40 | 38 |
| 14     | 27  | 35  | 17 | 17 | 19 | 22 | 17 | 16 |
| 15     | 49  | 64  | 36 | 36 | 47 | 55 | 28 | 31 |
| 16     | 32  | 30  | 24 | 24 | 18 | 24 | 20 | 25 |
| 17     | 56  | 46  | 35 | 32 | 44 | 34 | 38 | 38 |
| 18     | 59  | 44  | 36 | 32 | 77 | 77 | 80 | 75 |
| 19     | 51  | 57  | 42 | 44 | 39 | 47 | 37 | 41 |
| 20     | 48  | 48  | 11 | 12 | 28 | 36 | 20 | 19 |
| 21     | 25  | 42  | 11 | 12 | 13 | 19 | 10 | 14 |
| 22     | 41  | 38  | 24 | 29 | 16 | 15 | 20 | 28 |
| 23     | 69  | 75  | 51 | 47 | 55 | 62 | 52 | 53 |
| Mean (CI 95%) | 58 (44–71) | 59 (47–72) | 33 (24–42) | 33 (24–42) | 45 (34–55) | 47 (36–58) | 37 (27–47) | 39 (29–49) |
The average absolute percentage difference from mean tumor volume was significantly lower when using semi-automatic segmentation (14%, CI:9–19%) than when using manual segmentation (32%, CI: 26–37%, $p < 0.001$, Fig. 3). The percentage difference was significantly lower for squamous cell carcinoma compared to adenocarcinoma (23, 36%, $p < 0.05$) when using manual segmentation. This difference was not observed for semiautomatic segmentation.

**Discussion**

In comparison to manual segmentation, the use of semiautomatic segmentation resulted in a higher interobserver agreement and a lower average absolute percentage difference from mean volume when comparing esophageal tumors volumes segmented by consultant and resident radiologists.

The clinical and research values of CT volumetry at esophageal cancer management are controversial [8, 20, 21]. One possible reason behind this is the fact that CT volumetry...
technology and volumetry techniques used have not been sufficiently addressed and therefore may be suboptimal. For instance, small difference in image contrast between the tumor and the normal esophageal tissues may result in substantial variability in the final calculations. This variation is probably user and experience dependent. In this study, it was observed that the resident, but not the experienced radiologist, had a greater variation when manually delineating adenocarcinoma than squamous carcinoma. This might be explained by small differences in tumor texture [22], which are probably too small to allow the radiologist to diagnose tumor subtype. However, we have recently shown that computerized image analysis, so called CT morphometry, can distinguish between esophageal adenocarcinoma and squamous cell carcinoma [22]. Those small differences in texture might aid the experienced radiologist to better delineate adenocarcinoma but might be too small to the resident to discern. This would explain why the observed difference in tumor volume assessment varied between the resident and consultant radiologist differed between tumor subtype.

One study reported great variations in repeated measurements done by the same observer and also between expert radiologists using the manual segmentation approach [23]. In our study, we observed that by using a semiautomatic segmentation technique, we could significantly reduce this variation to the level of excellent agreement and making the measurements independent on the level of experience of the assessor. A recent study comparing different semiautomatic segmentation software has shown similar excellent intra- and inter observer agreement [24].

Different criteria have been used for the morphological evaluation of esophageal tumors, ranging from bi-dimensional measurement of tumor lesions according to the WHO criteria [25] to the thickness of the esophageal wall [20, 26] or assessment of the volume by use of stereology [27]. In our study, we used the summation-of-area method described by Breiman [28]. This is a simple method which does not require any sophisticated mathematical formulas and has been mainly used to assess the volume of solid organs such as the liver and spleen and also tumor masses e.g. head and neck and kidney.

The observed discrepancy between the readers when evaluating individual tumors can be attributed to several contributing factors. The main individual factor was probably the small difference in image contrast between the tumor and the normal esophageal tissue. This resulted in difficulties in defining the respective cranial and caudal borders of the tumors, especially in tumors located close to or at the gastro-esophageal junction. In addition, the current CT scans consisted only of axial images whereupon no multiplanar reformations were available to the readers. Thinner collimation and coronal and sagittal reformations may add to a better delineation of the cranial and caudal borders of the tumors. Other possible ways to improve the definition of the tumor borders can be to use positive or negative oral contrast media just prior to the CT examination and by the aid of antispasmodic agents [14, 29]. On the other hand, the introduction of a specific, more complex CT protocol for the study of the esophagus might be difficult to implement into clinical routine practice outside tertiary referral centers, where the esophageal tumors are examined with standard CT examinations in the N and M-staging process.

Other methods than CT can add to the armamentarium of methods allowing tumor volume detection and assessment of changes therein. PET-CT imaging with 18 FDG has recently been shown to offer advantages in monitoring the response to neoadjuvant treatment of esophageal cancer by measuring the metabolic/volume activity [21, 30, 31]. However, uncertainties regarding which thresholds of standardized uptake value (SUV) during the delineation of tumor remain as a source of variability in previous studies and there is currently no standardized protocol in use. Analysis of apparent diffusion coefficient (ADC) using diffusion-weighted magnetic resonance imaging (DWI-MRI) has been shown to correlate with histological tumor response and tumor staging [32–34]. The need to segment tumor volume in order to calculate ADC highlights the importance of reducing the interobserver variation of the tumor segmentation.

Recent developments of computing power have enabled quantification of textural parameters of tumor volumes segmented from both CT and PET images, which has been shown to correlate with overall survival and treatment response in several studies [35–37], but not in all [22]. However, these methods are sensitive to segmentation errors and accurate segmentation methods are needed in order to ensure comparable results between studies [38, 39].

There are some limitations burdening this study. The number of patients was relatively small and there were only two readers, which exposes the outcome to the risk of the random effect of single outliers. A further sub analysis of differences between segmentation methods depending on histological type might have not shown significance due to lack of enough patients per group (n = 15 versus n = 8). The patients were also scanned on two different scanners. However, this should not impact the comparison between semiautomatic and manual segmentation.

**Conclusions**

In conclusion, when compared to manual segmentation, application of semiautomatic CT volumetry of esophageal tumors obtained by using modern CT technology, reduces the interobserver variability, regardless of the observer's experience.
Abbreviations
CI: 95% confidence interval of the mean; CT: Computed tomography; DWI-MRI: Diffusion-weighted magnetic resonance imaging; FDG: Fluorine 18 fluorodeoxyglucose; ICC: Intraclass correlation coefficients; PET: Positron emission tomography; SUV: Standardized uptake value

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Availability of data and materials
The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

Authors’ contributions
YJ acquisition of data, analysis, interpretation, drafting the manuscript, final approval, accountable for all aspects of the work. MF conception and design, analysis, interpretation, drafting and revising the manuscript, final approval, agreed to be accountable for all aspects of the work. LL conception and design, drafting and revising the manuscript, final approval, agreed to be accountable for all aspects of the work. ÅJ conception and design, revising, final approval, accountable for all aspects of the work. IR acquisition of data, revising, final approval, accountable for all aspects of the work. TB conception and design, analysis, interpretation, drafting and revising the manuscript, final approval, agreed to be accountable for all aspects of the work. HL acquisition of data, analysis, interpretation, drafting and revising the manuscript, final approval, accountable for all aspects of the work. TB conception and design, analysis, interpretation, drafting and revising the manuscript, final approval, accountable for all aspects of the work. All authors have read and approved the manuscript.

Ethics approval and consent to participate
Ethical approval for the study was granted and the need for informed consent was waived by the regional ethical review board in Stockholm.

Consent for publication
Not applicable.

Competing interests
The authors declare that they have no competing interests.

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