Group Testing With Side Information via Generalized Approximate Message Passing

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Abstract—Group testing can help maintain a widespread testing program using fewer resources amid a pandemic. In a group testing setup, we are given \( n \) samples, one per individual. Each individual is either infected or uninfected. These samples are arranged into \( m < n \) pooled samples, where each pool is obtained by mixing a subset of the \( n \) individual samples. Infected individuals are then identified using a group testing algorithm. In this article, we incorporate side information (SI) collected from contact tracing (CT) into nonadaptive/single-stage group testing algorithms. We generate different types of CT SI data by incorporating different possible characteristics of the spread of disease. These data are fed into a group testing framework based on generalized approximate message passing (GAMP). Numerical results show that our GAMP-based algorithms provide improved accuracy.

Index Terms—Compressed sensing, contact tracing, generalized approximate message passing (GAMP), nonadaptive group testing.

I. INTRODUCTION

WIDESPREAD testing is a broadly used epidemiological tool for combating the COVID-19 pandemic. Samples are typically collected from nasal or oropharyngeal swabs and then processed by a reverse transcription polymerase chain reaction (RT-PCR) machine. However, widespread testing may be hindered by supply chain constraints and long testing times, especially at the inception of a pandemic.

Pooled or group testing has been suggested for improving testing efficiency [2], [3], [4], [5], [6], [7], [8], [9], [10], [11], [12], [13], [14], [15], [16], [17], [18]. Group testing involves mixing a subset of \( n \) individual samples into \( m < n \) pools. The measurement process can be expressed as \( y = \Omega(Ax) \), where \( x \) is a vector that quantifies the health status of the \( n \) individuals, \( A \) is an \( m \times n \) binary pooling matrix with \( A_{ij} = 1 \) if the \( j \)th individual contributes to the \( i \)th pool, else \( A_{ij} = 0 \), \( y \) is a vector of \( m \) noisy measurements or tests, and \( \Omega \) represents a probabilistic noise model that relates the noiseless pooled results, \( Ax \), to \( y \). Our work considers a noisy binary measurement model used by Zhu et al. [6], where \( x \) is a binary vector, \( w = Ax \) is an auxiliary (noiseless) vector, and the measurement \( y_i \in \{0, 1\} \) depends probabilistically on \( w_i \), where \( \mathbb{P}(y_i = 1 \mid w_i = 0) = 0 \) and \( \mathbb{P}(y_i = 0 \mid w_i > 0) \) are probabilities of erroneous tests.

We wish to estimate \( x \) from \( y \) and \( A \). We use single-stage nonadaptive algorithms as in [6], [8], rather than two-stage algorithms, which employ a second stage of tests depending on results from the first stage, as in Heidarzadeh and Narayanan [10] or the classical Dorfman approach [2]. Non-adaptive algorithms are advantageous in that they reduce testing time, which is high for RT-PCR.

Algorithms that estimate \( x \) from \( y \) and \( A \) [8], [12] rely primarily on the sparsity of \( x \), which is a valid assumption for COVID-19 due to low prevalence rates [19]. However, in addition to sparsity, the health status vector \( x \) contains plenty of statistical structure. For example, Zhu et al. [6] exploited probabilistic information such as the prevalence rate and structure in \( x \), and stated the potential benefits of using side information (SI). Specific forms of SI include individuals’ symptoms and family structure [1], [9]. Family structure refers to information regarding which individuals belong to the same family. Besides the conventional meaning of a family, within the context of disease spread, other types of family-like structure with significant contact between all individuals could include a group of students sharing the same room in a hostel, security officers working regularly at the same checkpoint, or healthcare workers working in the same facility. Finally, Nikolopoulos et al. [11], [16] independently observed that community structure can improve the performance of group testing; these works focused on encoder design in conjunction with basic decoders.

The focus of our work is on innovative decoder design. Our algorithmic approach for the decoder uses approximate message passing (AMP) [21], which has been proven to achieve the best-possible estimation quality in the large system limit for certain matrices [22], [23], [24]. Although the structured, binary, non-random measurement matrices that we use do not fall into
this category, nonetheless, it seems plausible that our numerical results with these matrices are favorable. Our AMP-based decoder is theoretically motivated, and therefore expected to estimate $x$ well, in particular for large problem sizes. The overarching message of our article is that using SI within AMP-based approaches can greatly improve group testing.

Contact tracing (CT) information has been widely collected and used for controlling a pandemic [25]. Such information, including the duration of contact between pairs of individuals and measures of physical proximity, can be collected using modalities such as Bluetooth [26], the global positioning system [27], manual inquiries by social workers [28], [29], and financial transaction data [27], [30]. Karimi et al. [31] used CT information to improve group testing using a loopy belief propagation (BP) algorithm.

In this article, we show how to estimate $x$ while utilizing CT SI. Our contributions are twofold. First, in Section IV, we propose group testing decoding algorithms based on generalized approximate message passing (GAMP) [32], and demonstrate how CT SI can be utilized. Our numerical results are presented in Section V; a typical result appears in Fig. 1. Our work uses more SI than other binary group testing algorithms [11], [16], [17] that only considered family/community structure in binary group testing when designing their encoders.

Our second contribution is to the AMP [21] community. The prior art has considered vector denoisers within AMP, within GAMP [33], and even SI-aided vector denoisers within AMP [34], including rigorous state evolution results [35], [36]. However, combining SI-aided vector denoisers within generalized AMP (GAMP) is new, to the best of our knowledge. GAMP adds another layer of complexity beyond AMP, hence combining these tools within GAMP could be numerically unstable. Our favorable numerical results suggest that fusing these algorithmic tools together offers a good direction for future work in SI-aided signal recovery.

We also mention that an extended online version of our work [37] incorporates SI at the encoder. We demonstrate numerically that SI at the encoder provides little extra performance benefits over the utilization of SI only at the decoder.

The rest of the article is organized as follows. In Section II, we survey related work. Our CT data is described in Section III. Our main contributions appear in Section IV, where we propose a GAMP-based group testing algorithm that exploits CT SI. Numerical results are presented in Section V. We discuss our findings in Section VI and conclude in Section VII.

II. RELATED WORK

Side information (SI) can be derived from many data sources, including travel history, medical history, and symptoms. SI can be used to assign infection probabilities as prior probabilities to individuals, who can subsequently be classified into different risk levels. Risk-aware group testing algorithms can then process individuals based on their risk levels.

This risk-aware approach has proven to be effective. For example, Deckert et al. [38] demonstrated a marked reduction in the number of tests required if pooling is performed on subjects with similar infection probabilities, as opposed to subjects with widely varying infection probabilities. Moreover, risk-specific algorithms can incorporate strategies to minimize the number of tests; McMahan et al. [39] adopt such a hierarchical approach in conjunction with classical Dorfman pooling [2], identifying pool sizes that minimize the expected number of tests. In broadly similar work by Bilder et al. [40], individuals are sorted per their infection probabilities, and extra tests are assigned for high-risk individuals.

There are also algorithms that make use of SI about family structures or contact tracing information. One recent example is our previous work with Zhu and Rivera [6], [9], who used both individual infection probabilities derived from symptom SI and family information while performing the decoding.

More recently, Nikolopolous et al. [11], [16] used SI about connected or overlapping communities to design good encoding matrices. The designed matrices boost the performance of basic decoders such as definite defectives (DD) [3] or loopy belief propagation (LBP) [41], in conjunction with a model for binary noise that resembles our model.

The work that is likely closest to ours is Karimi et al. [31]. Both works fully employ contract tracing SI in the decoder. Additionally, both works consider noisy measurements.

Ahn et al. [17] and Arasli and Ulukus [18] considered correlations represented by arbitrary graphs drawn from a stochastic block model, albeit for adaptive group testing, unlike the nonadaptive approach in this article. Their approaches

Fig. 1. Performance of the proposed group testing method with binary noise at four averaged sparsity levels and three measurement levels for a population of $n = 1000$ individuals. Our algorithms use family and contact tracing information to obtain false negative rates (FNR) and false positive rates (FPR) that are more appealing than those obtained by the prior art noisy-CoMa [20] and noisy-DD [3]. See Section V-B for more details. We also ran noisy-LiPo [20] with the same datasets, and it has larger FNR than noisy-DD.
generalized the i.i.d. assumption often used in group testing. Such correlations could be derived from family or contact tracing information. Graphs generated from this model contain node clusters with dense connections within a cluster and sparse connections between clusters. Such structures are typical of many social network graphs. The authors in [15], [42] provided an analytical proof of cost reduction in Dorfman pooling if there is a positive correlation between the different samples being pooled. Moreover, Lin et al. [13] also presented a hierarchical agglomerative algorithm for pooled testing in a social graph. We note that [13], [17], [18], [42] do not consider measurement noise.

Another approach was considered by Lau et al. [43]. They employ the Ising model to capture underlying structures and dependencies in the data. They solve the Ising model with quadratic and linear programming, resulting in performance improvements in group testing. Different from our work, CT information is captured by edge strengths in the Ising model.

The recent approach by Gatta et al. [44] fits a graph neural network to data on COVID-19 infections, deaths, and recoveries in a certain geographic location. This approach allows the authors to estimate temporally varying parameters of differential equations associated with a susceptible, exposed, infectious, and recovered (SEIR) model. While there are some similarities to our work, we have used parameters based on recent documents published by the World Health Organization (WHO) [38], whereas Gatta et al. [44] use a data-driven approach to perform regression via a graph-based neural network. Note that a neural network requires a large amount of data for training, which would not be readily available at the beginning of a pandemic. In contrast, our approach uses only basic knowledge about the spread of disease.

III. DATA GENERATION APPROACH

This section summarizes the main points of a data generation system that we use to illustrate a possible GAMP-based group testing decoding algorithm that uses CT. Our data generation system resembles the SEIR approach [45], [46], [47], but is not a contribution per se.

Below, we only present features of the data generation system that are utilized for algorithm design in Section IV. GAMP is more of an algorithmic framework than a single algorithm, and a specific GAMP approach is derived based on statistical information about the structure of the vector \(x\) and its dependence on CT information (Section IV). For these reasons, our data generation system was created merely to demonstrate the efficacy of this GAMP-based framework.

We model \(n\) individuals using a dynamic time-varying graphical model, where for each day dynamic undirected edges represent recent contacts between pairs of nodes, where nodes stand for individuals. Each node can be in one of four states, susceptible, infected, infectious, and recovered; for transitions between states, see Fig 2. CT applications are assumed to provide the decoder with SI in the form of \(\tau_{ij}^{(t)}\), the contact duration, and \(d_{ij}^{(t)}\), a measure of physical proximity. The infection probability is decided by the CT SI along with individuals’ viral load, \(x_i\), where only individuals in states infected or infectious have positive viral loads. More details about our data generation system appear in the Appendix.

IV. PROPOSED GROUP TESTING ALGORITHMS

This section describes a class of group testing algorithms that use side information (SI) within generalized approximate message passing (GAMP) [32] for reconstructing the health status vector \(x\) from the pooled tests, \(y\), given the pooling matrix, \(A\).

A. GAMP-Based Group Testing

Zhu et al. [6] use GAMP [32] for group testing estimation. GAMP is comprised of two components. The first component is comprised of an input channel that relates a prior for \(n\) individuals’ health status, \(\hat{x} = (x_i)_{i=1}^n\), to pseudo data,

\[
v = x + q \in \mathbb{R}^n, \quad (1)
\]

where the \(n\) coordinates of \(x\) are correlated, and \(q\) is additive white Gaussian noise with \(q_i \sim \mathcal{N}(0, \Delta_i)\). When the \(i\)th individual is in the infected/infectious state as defined in Fig. 2 and Section III, \(x_i = 1\); otherwise, \(x_i = 0\). The pseudo data \(v\) is an internal variable of GAMP that can be considered as a corrupted version of the true unknown health-status vector \(x\). The pseudo data is later iteratively cleaned up to gradually reveal \(x\). The unknown input \(x\) can be estimated from pseudo data \(v\) using a denoising function (or a denoiser):

\[
\hat{x}_i = g_{\text{in}}(v) = \mathbb{E}[X_i \mid V = v], \quad (2)
\]

where we use the convention that when both the capital and lower case versions of a symbol appear, the capital case is a random variable and the lower case is its realization, and \(\mathbb{E}[X_i \mid V = v]\) represents \(\mathbb{E}[X_i \mid V = v]\) when the context is clear.

The second component of GAMP is comprised of an output channel relating the auxiliary vector \(w\) to the noisy measurements \(y\) as reviewed in Section I. We adopt the output channel denoiser of Zhu et al. [6],

\[
h_j = g_{\text{out}}(y_j; k_j, \theta_j) = \frac{\mathbb{E}[W_j \mid y_j, k_j, \theta_j] - k_j}{\theta_j}, \quad (\theta_j) \text{ is the estimated variance of } h_j, \quad (k_j) \text{ is the mean of our estimate for } w_j. \quad \text{Since } y_j \text{ depends probabilistically on } w_j, \quad \text{we have } f(w_j \mid y_j, k_j, \theta_j) \propto \Pr(y_j \mid w_j) \propto \exp\left[ -\frac{(w_j - k_j)^2}{2\theta_j} \right], \quad \text{where } f \text{ is a probability density function}
\]
Algorithm 1: Pseudocode for the GAMP Framework.

Inputs: Maximum iterations \( t_{\text{max}} \), side information, probabilities of erroneous tests, measurements \( y \), and matrix \( A \).

Initialize: \( t, k, h_j, \theta_j, \tilde{x}_i, s_i \) \( \forall i \in [1, n], j \in [1, m] \).

Comment: \( t \) is iteration number, \( k \) is mean of our estimate for \( A x \), \( h_j \) is correction term for \( w_j \), \( \theta_j \) is variance of \( h_j \), \( \tilde{x}_i \) is our estimate for \( x_i \), and \( s_i \) is variance in our estimate \( \hat{x}_i \), and \( \circ \) is the Hadamard/elementwise product.

1: while \( t < t_{\text{max}} \) do
2: // clean up the output channel:
3: \( \theta = A \hat{\theta} - \theta \circ h \) // mean of \( u \) per previous iteration
4: \( k = A \hat{x} - \theta \circ h \) // mean of \( w \) per previous iteration
5: for \( j = 1 \) to \( m \) do
6: \( h_j = g_{\text{out}}(y_j; k_j, \theta_j) \)
7: \( r_j = -\frac{\partial}{\partial \sigma^2} g_{\text{out}}(y_j; k_j, \theta_j) \)
8: \( \Delta = [\frac{1}{2} (A^T A)^{-1}] \) // scalar channel noise variance
9: \( v = \hat{x} + \Delta \circ A^2 h \) // pseudo data
10: // clean up the input channel:
11: for \( i = 1 \) to \( n \) do
12: \( \hat{x}_i = g_{\text{in}}(v) = E[X_i | v] \) // conditional mean
13: \( s_i = E[X_i^2 | v] - E^2[X_i | v] \) // conditional variance
14: \( t = t + 1 \)

Output: \( \hat{x} \), pseudo data \( v \), and scalar channel noise variance \( \Delta \).

and \( W_j \) is approximated as Gaussian per the central limit theorem when there are enough ones in the \( j \)th row of pooling matrix \( A \). Our pseudocode for the GAMP framework is given in Algorithm 1. GAMP’s signal estimation quality is asymptotically optimal for large reconstruction problems, and it is also practically useful for finite problem sizes. Indeed, numerical results in Section V demonstrate that GAMP works adequately with a population \( n = 500 \) and well for \( n = 1000 \).

The key to an efficient GAMP-based estimator is the input-channel denoiser. While Zhu et al. [6] considered Bernoulli elements in \( x \) and alluded to supporting non-i.i.d. structure in \( x \) by using vector denoisers, this article provides details for probabilistic dependencies within \( x \). Below, we provide details for the design of two denoisers. Our first denoiser is based on a probabilistic model that considers groups of people, such as family members. Our second denoiser encodes the CT information into the prior for each individual’s health status.

B. Family Denoiser

We formalize a family-based infection mechanism, leading to a denoiser that improves detection accuracy. Define \( M_F \) as the set of indices of all members of family \( F \). We say that \( F \) is viral when there exists viral material in the family. Next, define the infection probability of individual \( i \) within a viral family \( F \) as \( \pi_{\text{ind}} = \mathbb{P}(X_i = 1 | F \text{ viral}) \), for all \( i \in M_F \), and \( \pi_{\text{f}} = \mathbb{P}(F \text{ viral}) \). Note that the infection status of individuals in a viral family are conditionally independent and identically distributed (i.i.d.).

Under our definition, family \( F \) being viral need not be attributed to any individual \( i \in M_F \). After all, viral material can be on an infected pet or contaminated surface. For this model, once the family is viral, the virus spreads independently with a fixed probability \( \pi_{\text{ind}} \). Of course, our simplified model may not accurately reflect reality. That said, without a consensus in the literature on how coronavirus or other infectious diseases spread, it is unrealistic to create a more accurate model. On the other hand, our model is plausible, and we will see that it is mathematically tractable. We further assume that individuals cannot be infected unless the family is viral, i.e., \( \mathbb{P}(X_i = 1 | F \text{ not viral}) = 0 \). The family structure serves as SI and allows the group testing algorithm to impose the constraint that people living together have strongly correlated health status.

Next, we derive the denoiser (2) by incorporating the family-based infection mechanism. Denote the pseudodata of the members of family \( F \) as \( x_F = (x_i)_{i \in M_F} \), the family-based denoiser for \( i \)th individual can be decomposed as follows:

\[
g_{\text{in}}(v_F) = \mathbb{E}[X_i | v_F] = \mathbb{P}(X_i = 1 | v_F) \] (3a)
\[
= \mathbb{P}(X_i = 1, F \text{ viral} | v_F) \] (3b)
\[
= \mathbb{P}(F \text{ viral} | v_F) \mathbb{P}(X_i = 1 | v_F, F \text{ viral}), \] (3c)

where the first term of (3c) is

\[
\mathbb{P}(F \text{ viral} | v_F) = \frac{f(v_F, F \text{ viral})}{f(v_F, F \text{ viral}) + f(v_F, F \text{ not viral})}. \] (4)

The two quantities in (4) can be further expanded as

\[
f(v_F, F \text{ not viral}) = (1 - \pi_{\text{f}}) f(v_F | F \text{ not viral}), \] (5a)
\[
= (1 - \pi_{\text{f}}) \prod_{i \in M_F} \mathcal{N}(v_i; 0, \Delta) \] (5c)

and

\[
f(v_F, F \text{ viral}) = \pi_{\text{f}} f(v_F | F \text{ viral}), \] (6a)
\[
= \pi_{\text{f}} \sum_{x_k \in \Omega_F} \prod_{i \in M_F} \left[ f(v_i | X_i = x_{k,i}) \mathbb{P}(X_i = x_{k,i} | F \text{ viral}) \right], \] (6b)

where \( \mathcal{N}(x; \mu, \sigma^2) := \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left(-\frac{(x-\mu)^2}{2\sigma^2}\right) \), and \( \Omega_F = \{0 \ldots 0, 0 \ldots 10, \ldots, 1 \ldots 11\} \) is a power set comprised of \( 2^{|M_F|} \) distinct infection patterns for family \( F \). The second term of (3c) can be simplified as follows:

\[
\mathbb{P}(X_i = 1 | v_F, F \text{ viral}) = \mathbb{P}(X_i = 1 | v_i, F \text{ viral}) \] (7a)
\[
= \mathbb{P}(X_i = 1, v_i | F \text{ viral}) / \mathbb{P}(v_i | F \text{ viral}) \] (7b)
\[
= \frac{\pi_{\text{ind}} \mathcal{N}(v_i; 1, \Delta)}{\pi_{\text{ind}} \mathcal{N}(v_i; 1, \Delta) + (1 - \pi_{\text{ind}}) \mathcal{N}(v_i; 0, \Delta)}. \] (7c)
\[
\begin{align*}
\pi_{\text{ind}} & = \frac{1}{\pi_{\text{ind}}} \cdot \mathcal{N}(v_i; 0, \Delta) \quad ^{-1} \quad (7d) \\
\pi_{\text{ind}} & = 1 + \left(\pi_{\text{ind}} - 1\right) \exp \left[\left(v_i - \frac{1}{\Delta}\right)\right]^{-1}. \quad (7e)
\end{align*}
\]

C. Contact Tracing Denoiser

While family structure SI characterizes part of the spread of the disease, individual family members will presumably all come in close contact with each other; hence CT SI will include cliques for these individuals. Additionally, CT SI describes inter-family contacts. Therefore, CT SI can characterize the spread of the disease more comprehensively than family SI.

Consider a hypothetical widespread testing program that relies on CT SI, where all individuals are tested 8 days before the testing program begins, resulting in a good initial estimate of their ground-truth health status. Note that our 8 d startup testing assumption is in line with China’s zero-Covid policy of testing large populations daily for weeks at a time [48]. To exploit the CT SI, we encode it for each individual i into the prior probability of infection, \(P(X_i = 1)\), and use the following scalar denoiser:

\[
g_{\text{CT}}(v_i) = \mathbb{E}[X_i | v_i] = P(X_i = 1 | v_i) \quad (8a)
\]

\[
f(v_i | X_i = 1) = \frac{P(X_i = 1)}{f(v_i)} \quad (8b)
\]

\[
\left(1 + \frac{\pi_{\text{ind}} - 1}{\pi_{\text{ind}}} \exp \left[\left(v_i - \frac{1}{\Delta}\right)\right]^{-1}. \quad (8c)
\]

Here, \(P(X_i = 1)\) for day \(k + 1\) can be estimated by aggregating CT information of individual \(i\) over a so-called SI period\(^1\) from day \(k - 7\) to day \(k\) as follows:

\[
P(X_i = 1) = \prod_{d=k-7}^{k} \left(1 - \hat{\lambda}_{i,j}^{(d)}\right), \quad (9)
\]

where \(\hat{\lambda}_{i,j}^{(d)}\) is the estimated probability of infection of individual \(i\) due to contact with individual \(j\). This probability, \(\hat{\lambda}_{i,j}^{(d)}\), may be determined by the CT information \((r_{i,j}^{(d)}, d_{i,j}^{(d)})\), as well as their infection status as follows:

\[
\hat{\lambda}_{i,j}^{(d)} = \exp \left(-\left(\lambda \tau_{i,j}^{(d)} d_{i,j}^{(d)} \Psi_{i,j}^{(d)} + \epsilon\right)^{-1}\right), \quad (10)
\]

where \(\Psi_{i,j}^{(d)} = 1 - \hat{\pi}_{i,j}^{(d)}(X_i = 0) \hat{\pi}_{i,j}^{(d)}(X_j = 0)\), \(\lambda\) is an unknown Poisson rate parameter, and \(\epsilon\) is used to avoid division by zero. We estimate \(\lambda\) with maximum likelihood (ML) using the pseudodata of all individuals, i.e.,

\[
\hat{\lambda}_{\text{ML}} = \arg\max_{\lambda} \prod_{i=1}^{n} f(v_i | \lambda), \quad (11)
\]

where \(f(v_i | \lambda) = f(v_i | X_i = 1) P(X_i = 1 | \lambda) + f(v_i | X_i = 0) P(X_i = 0 | \lambda)\). Once \(\hat{\lambda}_{\text{ML}}\) is obtained, it is plugged into (10) for calculating the prior probability in (9) [49]. As long as the pseudodata is not too noisy, the ML estimated parameter will be close to the true one, and the estimated probability \(\hat{\lambda}_{i,j}^{(d)}\) in (10) will be close to the true probability. This plug-in strategy can also be used for our family denoiser \(d_{\text{CT}}^{(\text{family})}(v)\), where \(\lambda = (\pi_{\text{ef}}, \pi_{\text{ind}})\).

V. NUMERICAL RESULTS

A. Experimental Conditions

The data were simulated based on the data generation process described in Section III, and group testing inference was performed using the algorithms proposed in Section IV. We call our family of algorithms GAMP-SI.

1) Experiment for \(N = 1000\): We generated datasets with \(n = 1000\) individuals using four levels of cross-clique contacts, leading to four averaged sparsity levels, 2.12%, 3.98%, 6.01%, and 8.86%, for \(x\).\(^2\) At each sparsity level, we perform pooling experiments using Kirkman triple matrices as proposed in [8] using \(m \in \{150, 300, 375\}\). Measurement vectors \(y\) for GAMP-SI were generated using probabilities for erroneous binary tests, \(P(y_i = 1 | w_i = 0) = 0.001\) and \(P(y_i = 0 | w_i > 0) = 0.02\), per Hanel and Thurner [51].

2) Experiment for \(N = 500\): We also generated datasets with \(n = 500\) individuals with averaged sparsity level 1.09%. Measurement vectors \(y\) for GAMP-SI were generated under the symmetric noise model, \(P(y_i = 1 | w_i = 0) = P(y_i = 0 | w_i > 0) = 0.01\), and 6 different pooling channel-coded matrices \((m \in \{100, 150, 200, 250, 300, 350\}\) were derived using a matrix design algorithm from Goenka et al. [37].

B. Main Numerical Results

We tested our model using both the family denoiser (3) and the CT denoiser (8).\(^3\) The top row of Fig. 1 summarizes the performance of GAMP-SI by choosing a representative operating point on an ROC curve, and Fig. 3 presents complete receiver operating characteristic (ROC) curves. Fig. 1 reveals that the CT denoiser outperforms the family denoiser in all settings. Both algorithms yield lower (better) FNR and FPR as the number of measurements, \(m\), increases. Moreover, the CT denoiser’s error rates are below 0.05, except for the challenging cases where the sparsity level is 8.86% and \(m \in \{150, 300\}\).

Fig. 3 illustrates the performance of family and CT denoisers at different measurement and sparsity levels. The circular dot on each curve is the operating point that minimizes the total error rate, i.e., the sum of FPR and FNR, which correspond to the concise results of Fig. 1. The closer a dot is to the origin of the FPR–FNR plane, the better the performance it reflects.

\(^1\) Owing to our 8 d startup testing assumption, starting the SI period on day \(k - 7\) and ending on day \(k\) lets us test on day \(k + 1\). Using this SI period for testing on day \(k + 1\) implicitly assumes that the test results are available within 24 hours. However, in cases when it takes more than 24 hours to generate test results, the SI period can be appropriately modified. For example, day \(k - 8\) to day \(k - 1\) for testing on day \(k + 1\) if it takes at most 48 hours to generate test results. After the testing program begins, we assume weekly testing, and probability estimates from the previous group test result 7 days before the current test are used as priors for the \(n\) individuals when performing the current group test.

\(^2\) Because the data generation model was used, it is difficult to control the average sparsity level from the underlying parameters. The sparsity level is measured after the data generation.

\(^3\) We have not included numerical results for the vanilla GAMP implementation without contact tracing SI, because we noticed some numerical instability in the challenging scenarios that involve low sparsity and low measurement rates. Of course, these are the interesting scenarios that group testing focuses on.
Comparing the ROC curves in the top and bottom rows, we note that the CT denoiser significantly outperforms the family denoiser at all sparsity levels. The CT denoiser, with most of its FNR and FPR $<5\%$, can achieve as low as $15\%$ of the total error rate of the family denoiser. Across different sparsity levels, the algorithm performs less accurately as the sparsity level increases. In each plot, lower measurement rates make it more challenging for the group testing algorithm.

We also examine the stability of the thresholds corresponding to the operating points we selected to report results in Fig. 1. Our empirical results reveal that at a given sparsity level, the variation of the threshold due to different design matrices or denoisers is less than 0.003. As the sparsity level increases from 2.12\% to 8.86\%, the threshold only drops from 0.160 to 0.137. Hence, the threshold for minimizing the total error rate is insensitive to the testing conditions.

We compare our proposed group testing algorithms to a baseline nonparametric belief propagation (NBP) algorithm [50] that does not exploit SI. We attach an additional output channel denoiser to the NBP algorithm to process the RT-PCR noise. We evaluate the performance in terms of FPR–FNR pairs and plot them using triangular markers in Fig. 3. Since the operating points are far from the ROC curves for GAMP using the family denoiser, we conclude that our proposed group testing algorithms that exploit SI outperform the NBP baseline that does not use SI.

GAMP-SI is also compared to the noisy Column Matching algorithm (No-CoMa), noisy LP Decoding algorithm (No-LiPo) [20], and noisy definite defectives (No-DD) [3] that do not exploit SI. No-LiPo and No-DD have large FNR levels, and No-CoMa is tuned for each sparsity level to minimize the sum of FPR and FNR for $m = 375$. We note that among all algorithms we are comparing with, No-CoMa performs the best and outperforms GAMP-family at the sparsity level 8.86\%. We believe the lower performance of GAMP-family at 8.86\% is caused by the mediocre SI provided as priors by the weekly group testing regime; we also observed that GAMP-family suffers from some numerical instability. In contrast to No-LiPo and No-DD having minimal FPR, GAMP-SI can offer any trade-off along the ROC curve.

We also compare GAMP-SI to belief propagation on combined graphs (BPCG) [31] that also employs cross-clique contact tracing as SI. Fig. 4 compares the performance of the two algorithms in an experiment for $n = 500$ individuals. For BPCG, we set the prevalence rate $p$ to 0.01, the contagion probability $q$ to 0.1 and the interaction probability $\theta$ to 0.008. The number of tests is set to be $m \in \{100, 150, 200, 250, 300, 350\}$. When $m$ is smaller, GAMP-SI has a higher success probability; this advantage vanishes as $m$ increases. With $m = 50$, GAMP-SI can still achieve a success probability of 0.702. Also, GAMP-SI
has a lower running time than BPCG. Specifically, for $n = 500$, BPCG takes around 680 seconds to produce the result of simulation of one day, on average, while GAMP-SI only takes around 16 seconds. Note that BPCG is designed to estimate samples’ states based on the information from the previous day; GAMP-SI can use the CT information from the entire previous SI period (multiple days).

### C. Additional Experiments

1) **Using Prior Knowledge of Infection Status:** We now examine the advantage that prior knowledge of the population’s infection status in the startup phase provides our algorithm for the model. As defined in (9), (10), we iteratively use the updated probability of infection, $\hat{P}(X_1 = 1)$, estimated from an SI period of 8 immediately preceding days. For days $k < 8$, we had to use the ground-truth infection status of each individual in the startup phase to generate the results reported in Section V-B.

However, ground-truth infection data from the startup phase may provide our approach an unfair advantage. Below, we investigate whether this advantage is significant. We examine how varying the amount of startup information impacts our algorithm’s quality. Specifically, we randomly replace a portion, $p_{\text{excluded}} \in \{0, 0.1, 0.5, 0.75, 1\}$, of the population’s infection status by an estimated probability of infection, e.g., 5%, for a setup that has a true averaged sparsity level of 7.2%. Using a probability instead of a binary value, 0 or 1, gives the algorithm soft probabilistic information instead of hard ground-truth style information.

Fig. 5 shows that even with 50% prior knowledge of the infection status of individuals, our detection accuracy for GAMP-SI is close to that when using complete startup information. The results show that the CT algorithm is robust to the absence of up to 50% of startup infection information, suggesting that the startup phase can likely be optimized to not require onerous testing resources.

2) **Duration of Startup SI Period:** It seems plausible to expect a trade-off between the accuracy of our algorithm and the amount of startup infection status data that needs to be collected before the initialization of our testing algorithm. We investigated numerically whether the accuracy of our algorithm is sensitive to the duration of the startup SI, or the startup SI period. We investigated the impact of the startup SI period by testing three durations, namely, 4, 8, and 12 days. The experiment was conducted on a sample of $n = 1000$ individuals with measurement rate $m/n \in \{0.1, 0.2, 0.3, 0.4\}$ at a sparsity level of 2.12%. Fig. 6 reveals that the estimation accuracy is not sensitive to the startup SI period. Specifically, as the startup SI period increases from 4 days to 8 days and then 12 days, the success probability increases by merely 0.01 and 0.005, respectively, at measurement rate 0.1. The increase in the success probability is even smaller when the measurement rate becomes larger. Therefore, we conclude that the startup SI period does not substantially impact the accuracy of our algorithm. For this reason, we chose 8 days as the startup SI period for the experiments conducted for this article.

### VI. DISCUSSION

Recent studies have shown that CT information based on Bluetooth may have privacy concerns, and contain many errors [27]. However, we note that there exist methods for obtaining CT information, which have been shown to be quite effective, including inquiries by social workers, cellphone-based localization, analyses of closed-circuit television footage, and financial transactions [28], [29], [30]. A fusion of these modalities can lead to more accurate CT data [27]. Contact tracing has been shown to be useful in previous epidemics [52]. As shown earlier, our algorithms are robust to errors in the CT SI. However, we leave a full-fledged investigation of SI errors and their impact on our algorithms to future work. We would like to point out that
at the peak of a pandemic, testing resources (including time, skilled manpower, testing kits, and reagents) could be scarce. In such a scenario, it is important to exploit as much information as is reasonably available in order to improve the performance of group testing algorithms, with the aim of saving critical testing resources.

VII. CONCLUSION

In this article, we have presented numerical evidence that side information (SI) from family structures and contact-tracing (CT) data can significantly improve the efficiency of group testing. The overarching message of our article is that using SI within AMP-based approaches works well.

There could exist other approaches that also incorporate SI at the encoder, in addition to the decoder considered here, resulting in further reconstruction improvements. However, we leave a full investigation of this aspect to future work.

Finally, due to the exploratory nature of our work and our deliberate efforts to bring algorithmic advances closer to practice, finding publicly available datasets with associated SI proved to be challenging. In light of this, we crafted a generative model that closely reflects the key characteristics of COVID-19 transmission for generating the data used in our investigation. Our numerical results present strong empirical evidence that CT supported group testing is a viable option to optimize the use of resources for a widespread testing program during a pandemic. Future work could consider a hybrid approach in which either the contact tracing data or infection status are real, and the other part of the data is simulated. Such an approach would be more realistic without requiring a significant data acquisition project.

APPENDIX

DATA GENERATION MODEL

In this section, we present a generative infection model that incorporates CT SI, which we use to prepare simulated data for algorithmic evaluation. We model a population of $n$ individuals using a dynamical (time-varying) graphical model that contains nodes, $\{u_i\}_{i=1}^n$, and undirected edges, $\{e_{ij}\}_{i,j=1}^n$. On a given day $t$, an edge $e_{ij}$ between nodes $u_i$ and $u_j$ encodes CT SI $(r_{ij}(t), d_{ij}(t))$, which can be acquired via Bluetooth-based CT applications [26]. Here, $r_{ij}(t)$ represents the contact duration and $d_{ij}(t)$ represents a measure of the physical proximity between individuals $i$ and $j$. On day $t$, a node can be in one of the following states: susceptible, infected, infectious, and recovered. Note that the infected state is defined in a narrow sense that excludes the infectious state, because states must be mutually exclusive. To keep the model simple, we assume that there are no reinfections, i.e., recovered is a terminal state, despite some reinfections [53]. While our model is inspired by a classical compartmental model in epidemiology comprised of susceptible, exposed, infectious, and recovered (SEIR) states considered for COVID-19 [54], our state transitions explicitly use CT SI and knowledge about the pandemic [55].

We adopt a simplified infection dynamic wherein the infectious period is preceded and followed by the infected state. Our design parameters for the infection dynamics are based on a WHO report on COVID-19 [55]. Specifically, a node $u_i$ remains infected but noninfectious for $k_1 = 3$ days. On day $t + k_1$, the node becomes infectious and may transmit the disease to a susceptible neighboring node $u_j$ with probability $p_{ij}$ whose construction is described below. An infectious node can potentially transmit the infection until $k_2 = 7$ days after getting infected, and becomes noninfectious afterward. Note that the above assumptions ensure that the transmission of infection on any given day is limited to one hop in the CT graph, i.e., it cannot be the case that individual $X$ infects individual $Y$, who in turn infects individual $Z$ on the same day. We also model a small fraction of stray infections that may occur, for example, due to sporadic contact with contaminated surfaces. Such infections only affect nodes in the susceptible state with a probability $p_1 = 2 \times 10^{-4}$ of our choice.

A state diagram appears in Fig. 2. Regarding the viral load $x_{ij}(t)$ for node $i$ on day $t$, we assume $x_{ij}(t) = 0$ if the node is susceptible or recovered. For an infected or infectious node, we make a simplified assumption that its viral load $x_{ij}(t) \sim \text{Uniform}(1, 2^{15})$, once drawn, remains constant throughout the combined 14-day period of infection.

Next, we model the probability $p_{ij}(t)$ that the disease is transmitted from node $u_i$ to $u_j$ on day $t$. We view infection times as a nonhomogeneous Poisson process with a time-varying rate function $\lambda(t)$. Consider a $r_{ij}(t)$-hour contact on day $t$ when susceptible node $u_i$ is exposed to infectious node $u_j$. The average infection rate $\lambda_{ij}(t)$ for day $t$ is assumed to be proportional to both the viral load $x_{ij}(t)$ and the physical proximity $d_{ij}(t)$, namely, $\lambda_{ij}(t) = \lambda_0 x_{ij}(t) d_{ij}(t)$, where $\lambda_0$ is a tunable, baseline Poisson rate. The probability that $u_j$ is infected by the end of contact period $r_{ij}(t)$ is therefore $p_{ij}(t) = 1 - \exp(-\lambda_0 x_{ij}(t) d_{ij}(t))$ for $t \in [k_1, k_2] + t_i$. From the standpoint of susceptible node $u_j$, all its neighbors $u_k$ that are infectious contribute to its probability of getting infected on day $t$, namely, $1 - \prod_{k \neq j}(1 - p_{kj}(t))$. We remark that if an individual catches the infection on day $t$, then it will possibly be detected only in testing conducted on the day $t + 1$, since we assume that sample collection and pooled testing is performed at the beginning of the day.

ACKNOWLEDGMENT

The authors thank Dr. Junan Zhu for allowing them to use and modify his implementation of GAMP with SI in their implementation of the family and CT denoisers. We also thank Karimi et al. [31] for kindly letting us use their implementation of BPCG.

4The cycle threshold for RT-PCR commonly ranges from 19 to 34 cycles [56, Fig. 3], where 34 cycles correspond to a low initial viral load of a few molecules, and each cycle roughly doubles the viral density. Therefore, we estimate the largest possible viral load as $2^{34} - 19 = 2^{15}$. 

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