Quantitative Normative Gait Data in a Large Cohort of Ambulatory Persons with Parkinson’s Disease

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Abstract

Background: Gait performance is widely evaluated to assess health status in older adult populations. While several investigators have presented normative values for spatiotemporal gait parameters drawn from older adult populations, the literature has been void of large-scale cohort studies, which are needed in order to provide quantitative, normative gait data in persons with Parkinson’s disease. The aim of this investigation was to provide reference values for clinically important gait characteristics in a large sample of ambulatory persons with Parkinson’s disease to aid both clinicians and researchers in their evaluations and treatments of gait impairment.

Methodology/Principal Findings: Gait performance was collected in 310 individuals with idiopathic Parkinson’s disease as they walked across a pressure sensitive walkway. Fourteen quantitative gait parameters were measured and evaluated with respect to Hoehn and Yahr disease staging and gender. Disease duration and age were controlled for in all analyses. Individuals with the greatest Parkinson’s disability walked significantly slower with shorter steps and stride lengths than the mild and moderately affected groups. Further, the most affected patients spent more time with both feet on the ground, and walked with a wider base of support than the moderately disabled patients. No differences were detected between the mild and moderate disability groups on any of the gait parameters evaluated.

Conclusions/Significance: Reference values for 14 gait parameters in a large cohort of ambulatory patients with Parkinson’s disease are provided and these may be highly useful for assessing and interpreting an individual’s gait dysfunction. It is important for clinicians and researchers to appreciate the lack of change in quantitative parameters as PD patients move from mild to moderate gait impairment.

Introduction

Gait impairment in Parkinson’s disease (PD) is often compounded by the presence of the other cardinal features of bradykinesia, rigidity, and postural instability. Individuals with PD typically exhibit a slow, short-stepped, shuffling gait with a forward-stooped posture and asymmetrical arm swing. These characteristics alter the metabolic efficiency of gait and lead to performance of routine walking near maximum capacity [1]. For most of us, independent functioning in the community is reliant upon the ability to walk efficiently. Thus, it is not surprising that gait impairment in PD is closely related to poor quality of life and to increased patient distress. Of note, patients themselves have been consistently documented to identify improvement in walking abilities as the most relevant outcome necessary to deem anti-parkinson treatment a success [2].
poral variables are not only relevant to defining gait performance, but may also be important indices relating to overall health.

If the movement disorders neurologist and rehabilitation specialist are to make judgments about the normality of a patient’s walking, reference values for clinically and functionally relevant spatiotemporal variables are required for comparison. While several studies have presented normative values of spatiotemporal gait data from healthy young and older adult populations [13–19], the literature is void of large-scale cohort studies that provide quantitative, normative gait data in PD. More common in the literature is a comparison of gait performance in a limited sample of persons with PD at various stages of the disease residing peers with similar age and gender characteristics. This is unfortunate, as this strategy provides limited clinical utility. Thus, the primary aim of this investigation was to provide reference values for clinically important gait characteristics in a large sample of ambulatory persons with PD at various stages of the disease.

Results

Demographic and clinical information for the sample is presented in Table 1. The quantitative gait parameters of our large cohort of patients are presented in Table 2. Individuals with the greatest Parkinson’s disability (severely disabled) walked significantly slower with shorter steps and stride lengths than the mild and moderately affected groups (Table 2; both p<0.01). Further, the percent of the gait cycle spent in stance was significantly greater in the more severely disabled group compared to their counterparts (Table 2, both p<0.05). Additionally, patients with moderate disability also spent more time in swing (Table 2, p=0.05), and narrower base of support (Table 2, p<0.001) compared to those in the severe disability group. Patients with moderate disability also spent more time in swing (Table 2, p<0.001) and less time in stance (Table 2, p<0.001) and time in double support (Table 2, p<0.001) than those with the highest disease burden. No differences were detected between the mild and moderate parkinsonian disability groups on any of the gait parameters evaluated.

A Gender main effect was also identified for numerous variables of interest (p<0.05). Male patients walked faster (1.00±0.02 m/s versus 0.77±0.03) with a faster cadence (103±1 step/min versus 98±2, p=.015) and produced larger steps (0.58±1 m versus.48±2, p<0.001) and stride lengths (1.17±2 versus.94±3, p<0.001). Further, male patients spent a significantly greater percent of the gait cycle in swing (34±2 versus 32±4, p=.01) and less in stance (66±3 versus 68±4, p=.01) than their female counterparts.

The component analysis revealed that three factors accounted for 89.3% of the variance in gait behavior. The first factor accounted for 45.0% of the variance in gait performance and was highly influenced by the temporal parameters including step time, swing time, single support time and percentage and double support time and percentage. In accordance with the work of Verghese et al. and Hollman et al. [12,18], we also termed this factor the rhythm factor. The second factor accounted for 35.8% of the variance loading primarily on velocity, step length, stride length and stance and swing % of the cycle. This factor has previously been coined the ‘pace factor’ [19]. The last factor encompassed 8.5% of the variance and loaded highly only on cadence and stance time.

Discussion

Our study provides normative values for widely used and clinically relevant gait parameters in ambulatory individuals with PD. These norms were derived at cross-section from a large and well characterized cohort of individuals. These comparative norms will help clinicians to compare the gait performance of an individual patient with idiopathic PD to a group of community-residing peers with similar age and gender characteristics. This is the first large population-based study to characterize in detail the relationships between Parkinsonian disability and a range of temporal and spatial gait measures.

Table 1. Patient Demographics.

| Age (years) | 68±10 |
| Disease Duration (years) | 8±6 |
| Sex | Male: 213 (68.7%); Female 97 (31.3%) |
| Handedness | Right: 90%; Left: 10% |
| Side of Onset | Right: 49%; Left: 41% Left; Both or unclear: 10% |
| Hoehn & Yahr | 2.2±0.6 |
| UPDRS Motor | 25.4±9.9 |
| PDQ Mobility | 31.5±27.3 |
| PDQ ADL | 28.9±21.5 |
| PDQ Emotional | 25.5±22.3 |
| PDQ Stigma | 17.3±21.1 |
| PDQ Social | 11.8±20.9 |
| PDQ Cognition | 27.8±20.8 |
| PDQ Communication | 25.8±23.0 |
| PDQ Discomfort | 34.1±23.3 |
| Schwab and England (patient) | 84.6±11.6 |
| Schwab and England (clinician) | 84.0±11.6 |

Values reported as mean ± one standard deviation.
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Slow gait speed is a significant predictor of poor clinical outcomes and has been associated with increased difficulties in performing activities of daily living, higher risk of falling, hospitalization, lower quality of life, and mortality.[13,20–22]. Due to the high relevance of gait speed, there have been several large-scale normative gait studies of gait speed in healthy older adult populations. Bohannon and colleagues [13] in a cohort of “younger” older adults (50–70 years, N = 121), reported comfortable gait speeds ranging on average from 1.35–1.39 m/s. With increasing age, self-selected walking speed is reduced. The mean gait velocity reported in several studies of community dwelling older adults older than 70 years of age range from 1.06–1.22 m/s. For example, Callisaya and colleagues [16] using similar methods and instrumentation to the present study, reported mean gait speeds averaging 1.16 m/s in men and 1.11 m/s in women from their population-based sample of 411 older adults (average age 72). Recently, in an older cohort of 800 participants (an average age of 80 years), Oh-Park and colleagues [19] documented a slower comfortable walking speed of 0.93 m/s. Of note, most of these studies have purposely excluded individuals with clinical gait abnormalities or diseases affecting gait such as Parkinson’s disease. In the present study, patients with PD walked with an average speed of 0.88 m/s, which is considerably slower than the healthy older adult values reported above. Moreover, as gait impairment in PD becomes clinically more pronounced with advancing disease, the slowest gait velocity is observed in those ambulatory patients with severe disability (Hoehn & Yahr Stages 3–4). Gait speed was on average 24% slower in ambulatory and severely disabled patients (Hoehn & Yahr Stages 3–4) compared to moderately disabled patients (stages <1.5 and 2–2.5). These reductions in gait speed have functional consequences. Forty percent of this cohort of people with Parkinson’s disease do not walk fast enough to cross a street before the light changes (i.e., <0.8 m/s), for instance. Further, in older adults survival decreases across the full range of gait speeds, with significant increments per 0.1 m/s [6].

Most studies across a wide range of ages suggest that men exhibit greater gait speed and stride length than women [16,18,19,23]. Our data were consistent with these findings. Gait speed in our cohort of males exceeded that of the females by approximately 22 m/s and stride length in men exceed that in women by approximately 22 m. However, similar to previous findings [18], if gait speed was normalized to stature (in this case leg length), the gender difference was no longer statistically significant. This post-normalization observation supports the notion that differences in gait speed are more influenced by body anthropometrics than by gender.

While gait speed is a well-accepted clinical screen, the magnitudes of other gait parameters also provide important clinical insight. Further, these variables may also be useful in predicting mobility disability and fall risk [11,24]. For example a 10% decrease from the normal 40% in the swing phase portion of the walking cycle, is associated with greater risk of falls [11]. In the present study of ambulatory patients with PD, the stance phase represented 66.5% of the gait cycle whereas the swing represented 33.5%. However, in the group of severely disabled females the swing phase portion encompassed 30% of the gait cycle, perhaps suggesting females with PD are at increased fall risk when compared to their male counterparts. Additionally, in our sample, double limb support occupied 35.1% and single limb support occupied 33.5% of the gait cycle. Comparatively, healthy older adults spend less time in double limb support (27.9% of cycle) and more time in single limb support (36.2% cycle) [18]. Moreover, on average persons in this study with a severe disability, Hoehn & Yahr stages 3–4, spent an additional 1.7% of the gait cycle in stance and 6.4% gait cycle in double support than previously reported in older adults [18,25]. This increase in stance and double support time represents a decreased efficiency of gait and thus a higher metabolic cost.

Callisaya et al [16] (mean age 72), Hollman et al [18] (ages 70–74, 74–79, 80–85) and Oh-Park et al [19] (mean age 80) provided normative data on cadence, step time, swing time, stance time,

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### Table 2. Gait Spatiotemporal Variables of Interest (values as reported as mean ±SD).

| VARIABLES | FEMALES ≤1.5 | 2–2.5 | 3–4 | MALES ≤1.5 | 2–2.5 | 3–4 | GROUP ≤1.5 | 2–2.5 | 3–4 |
|-----------|--------------|-------|-----|-------------|-------|-----|------------|-------|-----|
| Velocity (m/s) | 0.75±0.09 | 0.92±0.03 | 0.65±0.04 | 1.09±0.05 | 1.02±0.02 | 0.87±0.04 | 0.92±0.05* | 0.97±0.02* | 0.76±0.03 |
| Cadence (steps/min) | 96.4±3 | 105.2±2 | 94.2±2 | 104.2±2 | 103.1±1 | 101.2±1 | 100±2 | 104.1±1 | 97±1 |
| Step time(s) | 0.64±0.19 | 0.58±0.07 | 0.65±0.10 | 0.59±0.11 | 0.60±0.04 | 0.82±0.08 | 0.61±0.11 | 0.59±0.04* | 0.74±0.07 |
| Step Length (m) | 0.47±0.04 | 0.53±0.02 | 0.41±0.02 | 0.63±0.02 | 0.59±0.01 | 0.51±0.02 | 0.55±0.02* | 0.56±0.01* | 0.46±0.01 |
| Stride Length (m) | 0.95±0.08 | 1.05±0.03 | 0.83±0.04 | 1.25±0.04 | 1.19±0.02 | 1.04±0.03 | 1.10±0.05* | 1.12±0.02* | 1.04±0.03 |
| Step Width (m) | 0.10±0.01 | 0.09±0.01 | 0.12±0.01 | 0.11±0.08 | 0.10±0.01 | 0.12±0.01 | 0.10±0.01 | 0.10±0.01* | 0.12±0.01 |
| Swing (% cycle) | 32.0±1.2 | 34.2±0.4 | 30.6±0.6 | 34.6±0.6 | 34.0±0.2 | 33.2±0.5 | 33.3±0.7 | 34.1±0.2* | 31.9±0.4 |
| Swing time (s) | 0.41±0.05 | 0.40±0.02 | 0.40±0.02 | 0.40±0.03 | 0.40±0.02 | 0.45±0.03 | 0.41±0.03 | 0.40±0.01 | 0.42±0.02 |
| Stance (% cycle) | 68.0±1.2 | 65.8±0.4 | 69.4±0.5 | 65.4±0.6 | 66±0.2 | 66.8±0.5 | 66.7±0.6* | 65.9±0.2* | 68.1±0.4 |
| Stance time (s) | 0.87±0.05 | 0.77±0.02 | 0.92±0.02 | 0.76±0.03 | 0.78±0.01 | 0.83±0.02 | 0.81±0.03 | 0.77±0.01 | 0.87±0.02 |
| Single Support (% cycle) | 32.0±2.6 | 34.1±0.9 | 30.6±1.3 | 34.7±1.4 | 34.1±0.6 | 35.6±1.0 | 33.4±1.5 | 34.1±0.6 | 33.1±1.0 |
| Single Support time (s) | 0.41±0.05 | 0.40±0.02 | 0.40±0.02 | 0.40±0.03 | 0.40±0.01 | 0.45±0.02 | 0.41±0.03 | 0.39±0.01 | 0.42±0.02 |
| Double Support (% cycle) | 35.9±5.7 | 31.8±2.0 | 39.1±2.8 | 31.3±3.1 | 33±1.2 | 39.8±2.4 | 33.6±3.3 | 32.4±1.2* | 39.4±1.9 |
| Double Support time (s) | 0.46±0.25 | 0.37±0.08 | 0.52±0.12 | 0.37±0.13 | 0.39±0.05 | 0.69±0.10 | 0.42±0.14 | 0.38±0.05* | 0.61±0.10 |

*Statistically different from the severely disabled group (Hoehn and Yahr Stages 3–4). Values reported as mean ± one standard deviation. doi:10.1371/journal.pone.0042337.t002
stride length, and percent double support using the GAITRite system. Compared to the healthy older adult normative data in the literature, our persons with PD exhibited similar cadence, longer step times, reduced swing time, and greater stance time. Unfortunately, many of the other variables collected herein are mostly absent from the normative literature. Thus, our data will be useful as a reference to guide future investigations.

The results of our factor analysis build upon the findings expressed by Vergheese and colleagues [12] and more recently by Hollman and colleagues [18] in community dwelling healthy older adults. Each of these studies identified a “pace factor” typified by velocity and length measures. Pace-related parameters have been studied extensively among older adult populations as many of these variables directly relate to quality of life, fall risk, and even mortality. A second important factor identified in all three studies was a rhythm factor associated most closely with timing. However, parameters within the rhythm domain are also relevant as deleterious alterations in rhythm are related to risk of falling, mobility disability, gray matter atrophy [8] and increased risk of cognitive decline [12].

Several limitations are present and should be taken into account. Participants walked at their natural self-selected speed, not at their maximum possible. Thus, these norms may not relate to the total capacity of the individual. Second, all patients were tested while on anti-Parkinsonian medication. We did not however, standardize where in the medication cycle patients were at the time of testing. All patients self-reported that they were adequately responding to their medicine at the time of testing. This nested cohort study was necessarily restricted to those patients who received a gait assessment from April 2011-October 2011. This was a community based sample but persons were not recruited as a representative population sample. Data was not collected on matched healthy older adults for a direct comparison of the results to a similar community based sample of older adults. Subjects were consecutive patients at a tertiary care movement disorder center, and may or may not parallel the characteristics of a less optimized population. Proportionately, the sample is biased by a large cohort of moderately disabled patients (N=209) compared to the mild (N=31) and severe (N=70). On average 24±5.5 steps (12 strides) per participant were collected and analyzed. While there is support that measuring pace and rhythm parameters is highly reliable within this step range, reliability for other parameters, particularly in participants with high step variability, may be improved by evaluating data collected from hundreds of strides.

Conclusion

This study provides robust norms for quantitative gait parameters in a well-defined cohort of ambulatory community dwelling persons with Parkinson’s disease. These normative gait data are offered to help guide clinicians and scientist in evaluating and interpreting gait impairment.

Methods

Participants

Data were collected from three hundred and ten ambulatory patients with a diagnosis of idiopathic PD confirmed by a fellowship trained movement disorders neurologist. Data were collected in the medicated “on” state as part of their routine clinical exam at the Center for Movement Disorders and Neurorestoration in Gainesville, FL from April 2011-October 2011. Patients with deep brain stimulation or other Parkinson-related surgeries or dementia were excluded. The demographics of all participants can be found in Table 1. The study was approved by the University’s Institutional Review Board and all participants provided written informed consent prior to participating.

Equipment

Gait performance was measured while walking over the GAITRite instrumented walkway system (CIR Systems Inc., Havertown, PA). The 5.8 m × 0.9 m pressure sensitive walkway is composed of 18,432 sensors which were activated at foot contact and deactivated at toe-off. The walkway was centered within an isolated 12.2 m × 1.37 m collection hallway free from distraction. Data were collected at 120 Hz and processed within the GAITRite Platinum software. We evaluated data from 14 spatial and temporal gait parameters (Table 2).

Procedures

Participants performed four walks across the GaitRite walkway, beginning and terminating their walks at least 1.5 m before and after the pressure sensitive walkway to minimize acceleration effects. The participants were directed to walk at their natural comfortable pace. A verbal cue was provided to begin walking, though no other cues were provided during the walks nor was any feedback provided regarding their walking performance. Data from all four walks were combined.

A fellowship trained movement disorders neurologist administered part III of the Unified Parkinson’s disease Rating scale and determined the patients modified Hoehn and Yahr (H&Y) Staging. Additionally the Parkinson’s disease questionnaire (PDQ-39) and the Schwab and England (S&E) Disability Scale were completed. Disease duration was determined by subtracting the date of the evaluation from the date of diagnosis with idiopathic PD from the patient’s medical record.

Data Analysis

The dependent variables of interest (Table 2) were submitted to multivariate analysis of variance (MANOVA), comparing gender and Hoehn and Yahr disability group (Hoehn & Yahr stage ≤1.5, mild disability; Hoehn & Yahr stages 2-2.5, moderate disability; Hoehn & Yahr 3-4, severe disability) as independent variables while controlling for age and disease duration. The significance level for all tests was set at P≤.05. We attempted to characterize the gait performance of our participants using principal components factor analysis with varimax rotation. Factors with eigenvalues exceeding 1.0 and parameters with correlation loadings of 0.5 or higher were considered to be significant contributors to the observed behavior. All statistical tests were performed using SPSS 20 (IBM, Armonk, New York).

Author Contributions

Conceived and designed the experiments: CH JN AS IM MO NM. Performed the experiments: PM ES CJ. Analyzed the data: CH FM JN ES CJ. Contributed reagents/materials/analysis tools: CH AS IM MO NM. Wrote the paper: CH JN ES AS IM MO NM.

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