Implant-related artifacts around metallic and bio-integrative screws: a CT scan 3D Hounsfield unit assessment

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Abstract

Objective: To assess the degree of implant-related artifacts (IRA) around metallic and bio-integrative (BI) cannulated screws using Hounsfield units (HU) on computed tomography (CT). Our hypothesis was that BI implants would demonstrate significantly decreased IRA around the inserted screws.

Methods: In this cadaveric CT imaging study, we used 2 below-knee specimens. Medial displacement calcaneal osteotomy was performed, and the specimens were fixed with either metallic or BI screws. HU values were measured over 4 different lines that crossed the osteotomy position.

Results: The mean HU value was decreased in the BI implants compared to the metallic ones in 3 different positions: near the screw, directly over the screw, and inside the screw cannula. At the line placed 1 cm dorsal to the screw, the HU value for the metallic screw was lower than that for the BI screw.

Conclusions: We found metallic implants to demonstrate significantly increased HU values in regions close to the implant and significantly decreased values 1 cm away from the implant, when compared to the BI screw. The decreased HU values 1 cm away from the implant could be due to a shielding effect of the surrounding bone, hindering the assessment of union and healing. BI implants represent an alternative to decrease these IRA effects.

Level of Evidence III; Case Control Study.

Keywords: Osteotomy; Calcaneus; Metals; Radiography; Tomography, x-ray computed.

Introduction

Assessment of bone healing in osteotomies, fractures, and fusions has challenged orthopedic surgeons over the years12. Accurate bone visualization is important since healing parameters are used to determine postoperative protocols and the need for surgical revision56. Normally, both clinical and radiographic findings are the basis of this evaluation, as pain, site mobility, implant failure, and bone bridging are subjectively combined to support a decision towards union or nonunion56.

Computed tomography (CT) is widely regarded as the gold-standard imaging method when appraising bone healing78. When opposing bone surfaces have contiguous trabeculation or calcific density, union is characterized in that particular area78. To estimate the rate of bone healing, the amount of bone bridging is divided by the total contact surface9. Although a cut-off percentage for general ossification has not yet been established, when considering arthrodesis, values above 70% are usually designated as complete unions, and values between 33 and 69% are designated as partial unions9,10. Bone bridging above 25-49% in hindfoot and ankle arthrodesis has been correlated to good functional outcomes10.

Study performed at Department of Orthopedics and Rehabilitation, University of Iowa, Carver College of Medicine, Iowa City-IA, USA.

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Implant-related artifacts (IRA) represent a significant limitation in bone and soft tissue imaging evaluations\(^\text{12,13}\). When assessing bone healing through conventional CT, IRA may hinder a proper and complete judgment of bridging\(^\text{2,9}\). Metallic implants are the standard in foot and ankle surgery but are recognized as significant sources of IRA\(^\text{10}\). Absorbable and bio-integrative (BI) implants are attractive options for bone fixation when postoperative CT imaging is likely, particularly in procedures with a higher risk of nonunion. However, literature comparing the severity of IRA when using metallic or BI implants is scarce. The objective of this study was to compare the degree of IRA when using metallic vs BI cannulated screws. Our hypothesis was that BI implants would demonstrate significantly decreased IRA around the inserted screws when assessed by Hounsfield units (HU) on CT.

**Methods**

**Design**

This cadaveric, case-control study was performed at the Orthopedic Functional Research Imaging Laboratory (OFIRL), University of Iowa. Institutional Review Board approval was obtained (IRB# 202012422).

**Sample**

Two fresh-frozen cadaveric lower legs obtained from knee disarticulations were used. Specimens had no deformity and were thawed for 36 hours before experimental preparation\(^\text{15}\).

**Surgical procedure**

All surgical procedures were performed by a fellowship-trained foot and ankle orthopedic surgeon with more than 10 years of experience. Using a 5 cm traditional oblique lateral heel approach, medial displacement calcaneal osteotomies were performed on both specimens. A cut in the safe zone of the calcaneal tuberosity was done perpendicular to the lateral wall of the calcaneus and displaced medially by 10 mm\(^\text{16}\). It was then provisionally fixed with two parallel Kirschner wires under fluoroscopic guidance. Positioning and placement were checked in multiple planes. The wires were used for drilling and countersinking for a set of 4.0 mm cannulated headless screws.

One specimen received two 4.0 mm standard cannulated metallic (titanium) screws (Wright Medical\(^\text{®}\)), while the other received two 4.0 mm cannulated BI fiber screws (OSS lo\(^\text{®}\)). The BI screw is composed of 50% mineral fibers (silica, magnesium, calcium oxide, boron trioxide, phosphorus) and 50% polymer (poly [l-lactide-co-d, l-lactide])\(^\text{17}\). A hand screwdriver was used to place both sets of screws, and their placement was continuously monitored fluoroscopically during the procedure.

**Cadaveric model**

Cadavers were placed in an external frame after preparation of the proximal tibia. An 80 lb (356 N) axial load was applied to the construct. Muscle forces were applied to simulate a double-legged stance with the tibia approximately perpendicular to the floor. The tension of each muscle group was set relative to the peak contractile tension of the triceps surae’s strength, work percentage, and cross-sectional area. Muscle forces were then decreased proportionally to reflect axial loading to half body weight on each leg. The muscle forces applied to each tendon were: posterior tibial tendon (PTT), 40 N; flexor digitorum longus (FDL), 22 N; flexor hallucis longus (FHL), 22 N; peroneus brevis and peroneus longus combined, 35 N; and Achilles tendon, 200 N.

**Weight-Bearing CT (WBCT) measurement technique**

WBCT scans were performed with a cone-beam CT lower extremity scanner (HiRise; CurveBeam, LLC, Warrington, PA, USA). Raw multiplanar de-identified data were converted into sagittal, coronal, and axial plane images and evaluated using dedicated software (CubeVue\(^\text{TM}\), CurveBeam, LLC, Warrington, PA, USA). Assessments were performed by another board-certified foot and ankle surgeon with more than 10 years of experience who had experience with the dedicated software. The overall HU distribution within a 3D cube of 30 mm edge length was assessed. Additionally, within the cube, 4 linear projections were selected to sample the entire set of HU values along that line. Each line was parallel to the screws and crossed the osteotomy site. Line 1 was placed in close proximity to the screw (within 1 cm), Line 2 was placed directly over the screws, Line 3 was placed inside the screw cannula, and Line 4 was placed dorsal to the implant by 1 cm. The HU values on these lines were measured across the entire length of the line. Additionally, an 8 mm segment of each line as it crossed the osteotomy was selected (Figure 1).

**Statistical analysis**

For each measurement, data were evaluated for normality using the Shapiro-Wilk test, and descriptive statistics were obtained (mean, median, interquartile range [IQR], 95% confidence interval values). The average HU value for each line was compared between metallic and BI implanted specimens by t-tests/Wilcoxon analyses, and p-values ≤0.05 were considered significant. The JMP Statistical Software (SAS Institute\(^\text{®}\)) was used for the analysis.

**Results**

The specimen with metallic screws was found to have significantly higher HU values for lines 1, 2, and 3 when compared to the BI screw specimen. Values were significantly increased when considering both the entire line inside the 3D cube as well as the selected 8 mm line segment across the calcaneal osteotomy. When considering Line 1 (close to the screw), the metallic implant had higher HU values (entire, 7.26; selected, -5) when compared to BI (entire, -159; selected, -249). For Line 2 (over the top of the screw), the metallic implant was found to have higher HU values (entire, 4.84; selected, 6286) and the BI had lower values (entire, 108; selected, 151.2), as seen in figure 2. Line 3 (inside the cannula) was also found to have increased HU values for the metallic implant (entire, 1664; selected, 198.7) compared to the BI one (entire, 144; selected, -277.7). However, across Line 4 (1 cm away from the implant), HU values were significantly decreased around the metallic implant (entire, -49; selected, -110) compared to the BI implant (entire, 178.5; selected, 221), as seen in figure 3.
Figure 1. The left column shows data on the metallic implant and the right column, on the bio-integrative implant. Hounsfield unit distribution across Line 1 is represented by the yellow line, its distribution on Line 2 is shown by the purple line, that on Line 3, by the teal line, and that on Line 4, by the light blue line. The highlighted box 7.94mm across the graph shows the “selected” line segment.

Figure 2. Line 1 Hounsfield unit values for the whole line (A) and the selected line segment (B). Line 2 values for the whole line (C) and the selected line segment (D).
Discussion

Our cadaveric study demonstrated that BI implants significantly reduced HU values in 3 different planes across a calcaneal osteotomy: close to the screw, directly over the screw, and inside the screw cannula. Interestingly, HU values 1 cm away from the metallic screw (Line 4) were lower than those around the BI screw. This is potentially due to a beam hardening artifact, which might concentrate HU adjacent to the metal and shield the surrounding cancellous bone from being accurately reconstructed.

When assessing postoperative CT images for bone healing and the presence of nonunion, accurate diagnosis depends on having a clear scan close to the implant, as it crosses the osteotomy line. Historically, the lack of non-metallic implant options has led to IRA reduction through dual-energy CT scanners and post-CT imaging algorithms. Metal artifact reduction software (MARS) uses algorithms that aim to reduce the effect of beam hardening and photon starvation around the implant. While these methods can reduce IRA, allowing the surrounding tissue to be better visualized, they can also add streak artifacts close to the implant and are associated with data loss. BI implants have the possibility to remove the need for special CT protocols/software when imaging temporary hardware by reducing IRA. This could also lead to better scan quality around the implant, while saving resources on imaging and processing.

Recently, other non-metallic implant options have been used surgically in the form of biodegradable, magnesium screws. They have been shown to have significantly reduced IRA on postoperative CT scans and have similar efficacy to metallic implants. However, when magnesium is broken down in the body, hydrogen gas is released into the surrounding tissue. The gas does not cause clinical symptoms or affect fracture healing, but can be seen radiographically. More studies are needed to compare IRA when using magnesium and BI implants.

Some clear limitations of this study are the small number of specimens used and lack of implant diversity. This was a pilot study, and sample sizing and power analyses were not performed. Procedures that require more hardware in closer proximity might show differences in IRA reduction. In addition, the procedure was done on cadaveric specimens and HU measurements were completed immediately after; therefore, the change in IRA once the BI screws were allowed to integrate was not tested. Furthermore, the lack of a pre-ostectomy WBCT scan makes it difficult to assess the effect of BI screws on IRA. For a better assessment of IRA with BI screws, a pre-ostectomy HU assessment should be performed. No biomechanical testing was performed either. Surgeries and readings were each performed by different professionals, but only one surgeon and one reader were involved. WBCT and the software used for the assessments are not widely available, which could affect the study’s reproducibility.
Conclusions
In this study, we compared IRA around metallic and BI implants used to stabilize medial displacement calcaneal osteotomies. We found metallic implants to demonstrate significantly increased HU values close to the implant and significantly decreased values 1 cm away from the implant. This could be due to a shielding effect on the surrounding cancellous bone. These characteristics could potentially hinder the assessment of bone density quality and bone healing. Additional clinical studies are needed to confirm and expand our findings.

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