Pixel Detectors for Tracking and their Spin-off in Imaging Applications

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Abstract

To detect tracks of charged particles close to the interaction point in high energy physics experiments of the next generation colliders, hybrid pixel detectors, in which sensor and read-out IC are separate entities, constitute the present state of the art in detector technology. Three of the LHC detectors as well as the BTeV detector at the Tevatron will use vertex detectors based on this technology. A development period of almost 10 years has resulted in pixel detector modules which can stand the extreme rate and timing requirements as well as the very harsh radiation environment at the LHC for its full life time and without severe compromises in performance. From these developments a number of different applications have spun off, most notably for biomedical imaging. Beyond hybrid pixels, a number of trends and possibilities with yet improved performance in some aspects have appeared and presently developed to greater maturity. Among them are monolithic or semi-monolithic pixel detectors which do not require complicated hybridization but come as single sensor/IC entities. The present state in hybrid pixel detector development for the LHC experiments as well as for some imaging applications is reviewed and new trends towards monolithic or semi-monolithic pixel devices are summarized.

Key words: pixel detectors, semiconductor detectors, hybrid pixels, monolithic pixels, tracking, imaging

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1 Radiation hard hybrid pixel detectors for the LHC

An almost 10 year long development of pixel detectors for tracking close to the interaction point at the LHC was needed to develop pixel detector modules which meet the very high demands on spatial resolution, timing precision, long term operation performance and, most importantly, radiation tolerance to doses of as much as 500 kGy. All developments have been based on the *hybrid pixel technique*, in which sensor and FE-chips are separate parts of the detector module connected by small conducting bumps applied using the bumping and flip-chip technology. This technique is the only one which at present is robust and mature enough to cope with the above demands. All LHC-collider-detectors ALICE [1,2], ATLAS [3,4], and CMS [5,6], LHCb (for the RICH system) [7] at the LHC, BTeV [8] at the TEVATRON and the CERN fixed target experiment NA60 [9,10], employ the hybrid pixel technique to build large scale (up to \( \sim 2m^2 \)) pixel detectors. Pixel area sizes are typically 50\( \mu \)m \( \times \) 400\( \mu \)m as for ATLAS or 100\( \mu \)m \( \times \) 150 \( \mu \)m as for CMS. The detectors are arranged in cylindrical barrels of 2 to 3 layers and disks covering the forward and backward regions.

The discovery that oxygenated silicon is more radiation hard, with respect to the non-ionizing energy loss of protons and pions, [11] than standard silicon, allows operation of pixel detectors at the LHC for which the radiation is most severe due to their proximity to the interaction point. Sensors with \( n^+ \) electrodes in n-bulk material have been chosen to cope with the fact that type inversion occurs after about \( \Phi_{eq} = 2.5 \times 10^{13}\text{cm}^{-2} \). After type inversion the \( pn \)-diode sits on the electrode side thus allowing the sensor to be operated partially depleted. Figures 1(a) and (b) show the charge collection and the pixel pattern of the ATLAS pixel sensor [12]. Note the structures of a bias grid in the center of Fig. 1(b) which causes a drop of order 10% in the charge collection efficiency between pixel cells as shown in Fig. 1(a). This is considered tolerable in light of the benefit that the bias grid allows to test the sensors without a readout chip, an essential necessity for the building of large area detectors.

The challenge in the design of the front-end pixel electronics [13] can be summarized by the following requirements: low power (\(< 50\mu W\) per pixel), low noise and threshold dispersion (together \(< 200e\)), zero suppression in every pixel, on-chip hit buffering, and small time-walk to be able to assign the hits to their respective LHC bunch crossing. The pixel groups at the LHC have reached these goals in several design iterations using first radiation-soft prototypes, then dedicated radhard designs, and finally using deep submicron technologies. Figure 2 shows two recent wafer maps of ATLAS and CMS which demonstrate that radiation hard front-end chips with high yields in excess of \( \sim 80\% \) have been fabricated for the production of these LHC pixel detectors.
While CMS uses analog readout of hits up to the counting house, ATLAS obtains pulse height information by means of measuring the time over threshold (ToT) for every hit. Figure 3(a) shows the distribution of measured thresholds of an ATLAS front-end chip. The dispersion of about 600 e$^-\,$ can be lowered to below 50 e$^-$ by a 7-bit tuning feature implemented in the chip. Figure 3(b) illustrates the effect of time walk for small signals. For efficient signal detection within a defined time of 20 ns with respect to the bunch crossing an overdrive of about $1200e^-$ is necessary. The bunch crossing occurs every 25 ns.

The chip and sensor connection is done by fine pitch bumping and subsequent flip-chipping which is achieved with either PbSn (solder) or Indium bumps at a failure rate of $\lesssim 10^{-4}$. The Indium bumps are applied by a wet lift-off
Fig. 3. (a) Dispersion of the pixel thresholds before and after tuning. (b) In-time threshold and overdrive for a typical threshold setting of 4000±200e⁻.

technique and can be mated by direct thermo-compression [14,15] or reflowed, as developed by CMS [16]. After bumping the chips are thinned by backside grinding to a thickness of 150 - 180 μm. Fig. 4 shows rows of 50μm pitch bumps obtained by these techniques. All of these bump bonding technologies have been successfully used with 8” IC-wafers and 4” sensor wafers.

Fig. 4. (a) solder (PbSn, Photo IZM, Berlin) (b) Indium (Photo AMS, Rome), and (c) Indium with reflow (Photo PSI, Villigen) bump rows with 50μm pitch.

In the case of CMS and ATLAS a module (cf Fig. 5(a)) of typically 2 cm × 6.5 cm area consists of 16 FE-chips bump-connected to one silicon sensor. The I/O lines of the chips are connected via wire bonds to a kapton flex circuit glued atop the sensor. The flex houses a module control chip responsible for front end time/trigger control and event building. The total thickness at normal incidence is in excess of 2% X₀. The modules are arranged in barrel-ladders or disk-sectors as shown in Fig. 5(b).

The most challenging task in the pixel development for LHC was to meet the very high radiation dose that a pixel detector is exposed to during 10 years of operation (500 kGy). The advancement of oxygenated silicon and deep submicron chip technology made a long life time in such an environment possible. Figures 6(a)-(c) show the comparison of critical performance figures.
before and after irradiation of ATLAS pixel modules. In parts the received dose of the modules was well in excess of that expected for 10 years operation at the LHC. After irradiation to 500 kGy the mean collected charge fraction has been measured to be $87\pm14\%$ and the in-time efficiency, i.e. the efficiency for hit detection within 20ns after the bunch crossing, is 98.2%.

As the physics to be addressed with ALICE pixels is different from those addressed by ATLAS and CMS, a pixel module for ALICE has different key features. Because in ALICE the expected radiation is reduced ($<5$kGy, $6\times10^{12}n_{eq}$) cooling to temperatures below $0^\circ$C as for CMS and ATLAS is not mandatory. Very low total radiation length values are hence aimed for and achieved by the reduced cooling requirements (to $24^\circ$C), thus contributing only with $0.1\%X_0$, by a very light weight carbon fibre support structure ($0.1\%X_0$), and by using thin sensors (200 $\mu$m) and chips (150 $\mu$m). An ALICE module (1.28 cm $\times$ 7.0 cm) contains 5 readout chips bonded to one sensor. The total radiation length per layer is only $0.9\%$.

The CERN heavy ion experiment NA60 [10] has used LHC-type pixel detectors for the first time in a running experiment. The setup of the NA60 pixel tracker is shown in Fig. 7(a). For the initial running the ALICE-LHCb chip was used. Eight 4-chip (Fig. 7(b)) and eight 8-chip planes provide track reconstruction with 11 pixel hits on a track. In a recent run the sensors have been exposed to a radiation dose of 1.2 kGy and were operated through type inversion. Due to the inhomogeneous irradiation the inner part of the planes has received a larger dose than the outer, which is demonstrated by the hit multiplicity pattern taken with a lowered bias voltage in Fig. 7(c). The NA60 experiment has now upgraded the pixel detector by using original ATLAS pixel production modules.
Fig. 6. Comparisons of ATLAS pixel modules before and after irradiation to doses up to 100 Mrad. Hit map, noise and threshold dispersions (top), spatial resolution in the 50 µm direction of the pixels at 10° incidence angle (center), and the hit efficiency (bottom). The in-time efficiency of a hit to be earlier than 25 ns is determined in test beams relative to a fixed delay of the trigger counters. The highest point of the plateau shows the in-time efficiency. The width of the plateau characterizes the available margin during operation.
Fig. 7. Pixel detector tracker in the NA60 experiment (a) consisting of eight 8-chip planes and eight 4-chip planes (b). The pixel planes were operated through partial type-inversion, with the results demonstrated in the hit-multiplicity plot (c).

2 Imaging with Hybrid Pixel Detectors

Hybrid pixel detectors have had an impact on imaging applications as detectors that accumulate the incident radiation through the counting of individual radiation quanta in every pixel cell. This technique offers many features which are very attractive for X-ray imaging: full linearity in the response function, in principle an infinite dynamic range, optimal exposure times and a good image contrast compared to conventional film-foil based radiography (cf. Fig. 8). It thus avoids over- and under-exposed images. Counting pixel detectors must be considered as a very direct spin-off of the detector development for particle physics into biomedical applications. The analog part of the pixel electronics is in parts close to identical to the one for LHC pixel detectors while the periphery has been replaced by counting circuitry [17]. The same principle is also used for protein-crystallography with synchrotron radiation [18,19].

The challenges which are to be addressed in order to be competitive with integrating systems are: high speed (> 1 MHz) counting with a range of at least 15 bits, operation with very little dead time, low noise and particularly low threshold operation with small threshold dispersion values. In particular the last item is important in order to allow homogeneous imaging of soft X-rays of energies in the energy range below 10 keV. It is also mandatory for a differential energy measurement, realized so far as a double threshold with energy windowing logic [20,21,22], which can enhance the contrast of an image as the
Fig. 8. In comparison to X-ray imaging with film-foil systems imaging by counting can offer a linear response (a) and a very good image contrast without over and under exposure (b).

Fig. 9. (a) Image of a $^{57}$Co (122 keV $\gamma$) point source taken with a MEDIPIX2 counting single chip module (14x14 mm$^2$)[23], and (b) MPEC 2x2 multi chip module with a CdTe sensor[24].

The shape of the X-ray energy spectrum is different behind different absorbers (e.g. bone or soft tissue). Finally, for radiography, high photon absorption efficiency is mandatory, requiring the use and development of high Z sensors and their hybridization.

Several counting pixel system development efforts are being carried out: the MEDIPIX collaboration [25,22] uses the MEDIPIX chip with 256 $\times$ 256, 55 $\times$ 55$\mu$m$^2$ pixels fabricated in a 0.25$\mu$m technology, energy windowing via two tunable discriminator thresholds, and a 13 bit counter. The maximum count rate per pixel is about 1 MHz. Fig. 9(a) shows an image of a $^{57}$Co (122 keV $\gamma$) 1 mm diameter point source obtained with the Medipix2 SINGLE chip bonded to a 14x14 mm$^2$ CdTe sensor [23]. A Multi-Chip module with 2x2 chips using high-Z CdTe sensors with the MPEC chip [24] is shown in Fig. 9(b). The MPEC chip features 32$\times$32 pixels (200$\times$200$\mu$m$^2$), double threshold operation, 18-bit counting at $\sim$1 MHz per pixel as well as low noise values ($\sim$120$e$ with
CdTe sensor) and threshold dispersion (21e after tuning) [26,24]. A technical issue here is the bumping of individual die CdTe sensors which has been solved using Au-stud bumping with In-filling [27]. A challenge for counting pixel detectors in radiology is to build large area detectors. Commercially available integrating pixellated systems such as flat panel imagers [28,29,30,31,32] set the competition level.

In protein crystallography with synchrotron radiation [18] the challenge is to image many thousands of Bragg spots from X-ray photons with energies of \( \sim 12 \text{ keV} \) (corresponding to resolutions at the 1Å range) or higher, scattering off protein crystals. This must be accomplished at a high rate (\( \sim 1-1.5 \text{ MHz/pixel} \)) and by systems with a high dynamic range. The typical spot size of a diffraction maximum is \( 100-200 \mu m \), calling for pixel sizes in the order of \( 100-300 \mu m \). The high linearity of the hit counting method and the absence of so-called ”blooming effects”, i.e. the response of non-hit pixels in the close neighborhood of a Bragg spot, makes counting pixel detectors very appealing for protein crystallography experiments. A systematic limitation and difficulty is the problem that homogeneous hit/count responses in all pixels, also for hits at the pixel boundaries or between pixels where charge sharing plays a role must be maintained by delicate threshold tuning (cf Fig. 10(b)). Counting pixel developments are made for the ESRF (Grenoble, France) [33,34] and the SLS (Swiss Light Source at the Paul-Schererrer Institute, Switzerland) beam lines. A photograph of the PILATUS 1M detector [35] at the SLS (\( \sim 10^6 \) \( 217\mu m \times 217\mu m \) pixels, 18 modules, \( 20 \times 24 \text{ cm}^2 \) area) is shown in Fig. 10 (top photograph). It is the first large scale hybrid pixel detector in operation. Fig. 10(c) shows some Bragg spots obtained from a Lysozyme crystal with a 10s exposure to 12 keV synchrotron X-rays [36]. Some spots are contained in only one pixel, others spread over a few pixels due to charge sharing. This demonstrates the intrinsically good point resolution of the system. Alternative developments which aim to improve the active/inactive area ratio for protein-crystallography X-ray detection are so-called 3-D silicon sensors (strip or pixels) [37]. A detailed account can be found in [38].

3 New directions with Hybrid Pixel Detectors

To further develop Hybrid Pixel detectors for use in specialized applications and to improve in certain areas, several ideas and developments are being pursued.
Fig. 10. (top) Photograph of the 20x24 cm$^2$ large PILATUS 1M detector for protein crystallography using counting hybrid pixel detector modules, (bottom left) delicate threshold tuning with counting pixel detectors at the borders in between pixels, (bottom right) Bragg spots of an image of Lysozyme taken with PILATUS 1M [36] are often contained in one pixels.
Diamond Pixels

The successful development of radiation hard CVD-diamond sensors [39] with charge collection distances approaching 300 µm has triggered the developments of a hybrid pixel detector using diamond as sensors [40]. The non-uniform field distribution inside CVD-diamond, which originates from the grain structure in the charge collection bulk, leads to charge trapping at the grain boundaries [41] and – as a result – to shift in the position of reconstructed hits of the order of 100µm - 150µm. Diamond pixel detectors are well suited to study this effect [41]. Single chip pixel modules using ATLAS front-end electronics have been built and tested in a high energy (180 GeV) pion beam. Figure 11(a) shows the diamond pixel detector, Fig. 11(b) is a hit response pattern obtained by exposing the detector to a $^{109}$Cd source of 22 keV $\gamma$ rays, which deposits approximately 1/4 of the charge of a minimum ionizing particle. This demonstrates the good charge collection efficiency obtained. Diamond sensors with charge collection distances in in excess of 300 µm have been fabricated and tested [42]. Figure 11(c) and (d) show position correlation and the charge distribution of the diamond pixel detector in a high energy beam, respectively. A spatial resolution of $\sigma = 22\mu m$ has been measured with 50µm pixel pitch, compared to about 12µm with Si pixel detectors of the same geometry using the same electronics, revealing the influence of the mentioned position shifts.

HAPS

In order to achieve smaller pixel implant pitches with relaxed readout cell pitches capacitive coupling between pixels can be exploited as is done in the HAPS (Hybrid (Active) Pixel Sensors) concept [43]. This technique is adopted from capacitively coupled silicon micro strip detectors. The ratio of the number of interleaved to read-out pixels can be as large as 22/3 [43]. The charge accumulated on interleaved pixels couples via inter-pixel capacitances to the pixel cells which are read out. The implant pitch is designed for best spatial resolution using charge sharing between neighbors, while the readout pitch is tailored to the size needs of the front-end electronics cell. In this way resolutions between 3µm and 10µm can be obtained with pixel (readout) pitches of 100µm (200µm) [43].

MCM-D

The present hybrid-pixel modules of the LHC experiments use an additional flex-kapton fine-print layer on top of the Si-sensor (Fig. 12(a)) to provide power
Fig. 11. (a) Single chip diamond pixel module using ATLAS front-end electronics, (b) hit map obtained by exposure to a $^{109}$Cd radioactive source (22 keV $\gamma$), (c) scatter plot of position correlation between the diamond pixel detector and a reference beam telescope, and (d) measured Landau distribution in a CVD-diamond pixel detector.

and signal distribution to and from the module front-end chips. An alternative to the flex-kapton solution is the so-called Multi-Chip-Module Technology deposited on Si-substrate (MCM-D) [44]. A multi-conductor-layer structure is built up on the silicon sensor. This allows all bus structures to be buried in four layers in the inactive area of the module thus avoiding the kapton flex layer and any wire bonding at the expense of a small thickness increase of 0.1% $X_0$ (Fig. 12(b)). The extra freedom in routing also allows the design of pixel detectors which have the same pixel dimensions throughout the sensor. Fig. 12(c) shows the shows a scanning electron microphotograph (courtesy IZM, Berlin) of an MCM-D via structure, and Fig. 12(d) shows the photograph of an assembled ATLAS MCM-D module [45].
4 Monolithic and Semi-Monolithic Pixel Detectors

Monolithic pixel detectors, in which amplifying and logic circuitry as well as the radiation detecting sensor are one entity, are in the focus of present developments. To reach this ambitious goal, optimally using a commercially available and cost effective technology, would be another breakthrough in the field. So far it has not been completely reached and compromises are made. The present developments have been much influenced by R&D for vertex tracking detectors at future colliders such as the International Linear $e^+e^-$ Collider (ILC) [46]. Very low ($\ll 1\% X_0$) material per detector layer, small pixel sizes ($\sim 20 \mu m \times 20 \mu m$) and a high rate capability ($80 \text{ hits/mm}^2/\text{ms}$) are required, due to the very intense beamstrahlung of narrowly focussed electron beams close to the interaction region, which produce electron positron pairs in vast numbers. High readout speeds with typical line rates of 50 MHz and a 40$\mu$s frame time are necessary.

To classify the different monolithic approaches some distinctions can be made by posing the following questions:

- does the device allow full CMOS circuitry ? also in the active sensor area ?
is the charge collection performed in a fully depleted bulk providing a large signal?

does the processing technology employ a standard process or are specialized (non-commercial) technologies necessary?

The above mentioned ultimate monolithic goal would be fulfilled with a full CMOS commercial standard device with charge collection in a fully depleted bulk.

The present developments can then be characterized accordingly.

- Non-standard CMOS on high resistivity bulk
  The first monolithic pixel detector was successfully operated in a particle beam already in 1992 [47] using a high resistivity p-type bulk p-i-n detector in which the junction had been created by an n-type diffusion layer. On one side, an array of ohmic contacts to the substrate served as collection electrodes. Due to this, only pMOS transistor circuits sitting in n-wells were possible to be integrated in the active area. The technology was certainly non-standard and non-commercial. No further development emerged.

- CMOS technology with charge collection in epi-layer
  In some CMOS technologies a lightly doped epitaxial silicon layer of a few to 15$\mu$m thickness between the low resistivity silicon bulk and the planar processing layer can be used for charge collection [48,49,50]. The generated charge is kept in a thin epi-layer atop the low resistivity silicon bulk by potential wells at the boundary and reaches an n-well collection diode by thermal diffusion (cf. Fig. 13(a)). The sensor is depleted only directly under the n-well diode. The signal charge is hence very small ($<$1000e) and mostly incomplete; low noise electronics is the challenge in this development. As a pay-off, the fabrication of such pixel sensors is potentially very cheap. With small pixel cells collection times in the order of 100 ns - 150 ns are obtained. Despite using CMOS technology, the potential of full CMOS circuitry in the active area is not available (only nMOS) because of the n-well/p-epi collecting diode which does not permit other n-wells. CMOS monolithic active pixel sensors are similar to CMOS camera chips, but they are larger in area and must have a 100% fill factor for efficient particle detection. The epi-layer is – technology dependent – at most 15$\mu$m thick and can also be completely absent. Collaborating groups around IReS&LEPSI [51,52], RAL [53], Irvine-LBNL-Ohio [54], and Hawaii-KEK [55] use similar approaches to develop large scale CMOS active pixels also called MAPS (Monolithic Active Pixel Sensors) [49]. Prototype detectors have been produced in 0.6$\mu$m, 0.35$\mu$m and 0.25$\mu$m CMOS technologies [56,57].

  Matrix readout of MAPS is performed using a standard 3-transistor circuit (line select, source-follower stage, reset) commonly employed by CMOS matrix devices, but can also include current amplification and current mem-
Fig. 13. (a) principle of an Monolithic Active Pixel Sensor (MAPS) [49] targeting CMOS electronics with low resistivity bulk material. The charge is generated and collected by diffusion in the very few µm thick epitaxial Si-layer. (b) MAPS detector with 100 nm thin backside entrance window.

ory [56]. For an image two complete frames are subtracted from each other (CDS) which suppresses switching noise. Noise figures of 10-30e and S/N ~20 have been achieved with spatial resolutions below 5µm. Regarding radiation hardness MAPS appear to sustain non-ionizing radiation (NIEL) to $\sim 10^{12} n_{eq}$ while the effects of ionizing radiation damage (IEL) are at present still under investigation. The present focus of further development lies in making larger area devices for instance by stitching over reticle boundaries [57], increasing the charge collection performance in the epi-layer by triple-well [53], photo-gate [58], and photo-FET [56,52] techniques and developing a higher radiation tolerance. In addition, for applications like e.g. precise beam position monitoring in hadron therapy, devices with very thin entrance windows are needed to detect $\sim$20 keV electrons scattering off a thin metal foil held in a hadron beam. Such a thinned MAPS detector, which is also capable of autoradiographic tritium detection, is shown in Fig. 13 (b).

Above all, the advantages of a fully CMOS monolithic device relate to the adoption of standard VLSI technology and its resulting low cost potential ($\sim 25$ per cm²). In turn the disadvantages are also largely related to the dependence on commercial standards. The thickness of the epi-layer varies for different technologies. It is thinner for processes with smaller structure sizes and along with this also the signal decreases. Only a few processing technologies are suited. With the rapid change of commercial process technologies this is an issue of concern. Furthermore, as already stated, in the active area, due to the n-well collection diode, only nMOS circuitry is possible. The voltage signals are very small ($\sim$mV), of the same order as transistor threshold dispersions requiring very low noise VLSI design. The radiation tolerance of CMOS pixel detectors for particle detection beyond $10^{12} n_{eq}$ is still a problem although the achieved tolerance should be well sufficient for use in a future Linear Collider environment. Improved read-out concepts and device development for high rate particle detection at a linear collider are under development [46]. Concrete project planning to use CMOS active pixels in real experiments are the upgrades to the STAR mi-
cro vertex detector [56] and to the Super Belle detector (innermost layer) at KEK, for which very encouraging prototype developments and results have been presented at this conference [55].

- **CMOS on SOI (non-standard)**
  In order to exploit high resistivity bulk material, the authors of [59] develop pixel sensors with full CMOS circuitry using the Silicon-on-Insulator (SOI) technology. The connection to the charge collecting bulk is done by vias (Fig. 14(left)). The technology offers full charge collection in 200–300µm high resistive silicon with full CMOS electronics on top. At present the technology is however definitely not a commercial standard and the development is still in its beginnings. More details on this interesting new technology has been reported at this conference and can be found in [60].

![CMOS on SOI diagram](image)

Fig. 14. (left) Cross section through a monolithic CMOS on SOI pixel detector using high resistivity silicon bulk insolated from the low resistivity CMOS layer with connecting vias in between [61,59], (right) cross section through a structure using amorphous silicon on top of standard CMOS VLSI electronics [62,63].

- **Amorphous silicon on standard CMOS ASICs**
  Hydrogenated amorphous-Silicon (a-Si:H), where the H-content is up to 20%, can be put as a film on top of CMOS ASIC electronics. a-Si:H has been studied as a sensor material long ago and has gained interest again [62,63] with the advancement in low noise, low power electronics. The signal charge collected in the <30µm thick film is in the range of 500-1500 electrons. A cross section through a typical a-Si:H device is shown in Fig. 14(right). From a puristic view it is more a hybrid technology, but the main disadvantage, the hybridization connection, is absent. The radiation hardness of these detectors appears to be very high >10¹⁵cm⁻² due to the defect tolerance and defect reversing ability of the amorphous structure and the larger band gap (1.8 eV). The carrier mobility is very low (µₑ = 2-5 cm²/Vs, µₕ = 0.005 cm²/Vs), i.e. essentially only electrons contribute to the signal. Basically any CMOS circuit and IC technology can be used and technology changes are not critical for this development. For high-Z applications polycrystalline HgI₂ constitutes a possible semiconductor film material. The
potential advantages are small thickness, radiation hardness, and low cost. The development is still in its beginnings and – as for CMOS active pixel sensors – a real challenge to analog VLSI design.

- **Amplification transistor implanted in high resistivity bulk**

  In so-called DEPFET pixel sensors [64] a JFET or MOSFET transistor is implanted in every pixel on a sideways depleted [65] bulk. Electrons generated by radiation in the bulk are collected in a potential minimum underneath the transistor channel thus modulating its current (Fig. 15). The bulk is fully depleted rendering large signals. The small capacitance of the internal gate offers low noise operation. Both together can be used to fabricate thin devices. The sensor technology is non-standard and the operation of DEPFET pixel detectors requires separate steering and amplification ICs.

![Diagram of DEPFET pixel structure](image)

**Fig. 15.** Principle of operation of a DEPFET pixel structure based on a sideways depleted detector substrate material with an imbedded planar field effect transistor. Cross section (left) of half a pixel with symmetry axis at the left side, and potential profile (right).

The DEPFET detector principle is shown in Fig. 15. Sideways depletion [65] provides a parabolic potential which has – by appropriate biasing and a so-called deep-n implantation – a local minimum for electrons (∼1µm) underneath the transistor channel. The channel current can be steered and modulated by the voltage at the external gate and - important for the detector operation - also by the deep-n potential (internal gate). Electrons collected in the internal gate are removed by a clear pulse applied to a dedicated contact outside the transistor region. The very low input capacitance (∼few fF) and the in situ amplification makes DEPFET pixel detectors very attractive for low noise operation [66]. Amplification values of 400 pA per electron collected in the internal gate have been achieved. Further current amplification and storage enters at the second level stage.

DEPFET pixels are currently being developed for three very different application areas: vertex detection in particle physics [67,68], X-ray astronomy [69] and for biomedical autoradiography [66]. With round single pixel structures noise figures of 2.2e at room temperature and energy resolutions of 131 eV for 6 keV X-rays have been obtained [68]. With small (20x30 µm²)
linear structures fabricated for particle detection at a Linear Collider (ILC) the noise figures are about 10e. The spatial resolution in matrices operated with 50 kHz line rates is $[68,66] \sigma = (4.3 \pm 0.8) \mu m$ (57 LP/mm) for 22 keV $\gamma$ and $\sigma = (6.7 \pm 0.7) \mu m$ (37 LP/mm) for 6 keV $\gamma$. The capability to observe tritium in autoradiography applications has been demonstrated [66,68].

Fig. 16. (top) Sketch of a ILC first layer module with thinned sensitive area supported by a silicon frame. The enlarged view show a DEPFET matrix and a DEPFET double pixel structure, respectively, (bottom) photo of a DEPFET matrix readout system for LC applications. The sequencer chips (SWITCHER II) for select and clear are placed on the sides of the matrix, the current readout chip (CURO II) at the bottom.

The very good noise capabilities of DEPFET pixels are very important for low energy X-ray astronomy and for autoradiography applications. For particle physics, where the signal charge is large in comparison, this fea-
ture is used to design very thin detectors (∼50µm) with very low power consumption when operated as a row-wise selected matrix [70,68]. Thinning of sensors to a thickness of 50µm using a technology based on deep anisotropic etching has been successfully demonstrated [71]. For the development of DEPFET pixels for a Linear Collider, matrix row rates of 50 MHz and frame rates for 520x4000 pixels of 25 kHz, read out at two sides, are targeted. Sensors with cell sizes of 20x30µm² have been fabricated and complete clearing of the internal gate, which is important for high speed on-chip pedestal subtraction, has been demonstrated [68]. A sketch of a first layer module made of DEPFET sensors is shown in fig. 16(top). A large matrix is readout using sequencer chips for row selection and clear, and a column readout chip based on current amplification and storage [70,68]. Both chips have been developed at close to the desired speed for a Linear Collider. Figure 16(bottom) shows a DEPFET pixel matrix readout system suited for readout speeds at the ILC. The estimated power consumption for a five layer DEPFET pixel vertex detector at the ILC is only 5W. This assumes a power duty cycle of 1:200 and no power consumption of the SWITCHER chip in the off state. Such a performance renders a very low mass detector without cooling pipes feasible. The most recent structures use MOSFETs as DEPFET transistors for which the radiation tolerance still has to be investigated.

5 Summary

The Hybrid Pixel technology, in which sensor and electronic chip are separate entities connected via bump bonding techniques, has shown the way to large area (∼m²) pixel detectors for experiments at the LHC. These detectors are in construction and the maturity of the technology, including radiation tolerance to 500 kGy doses, has been proven. New developments include interleaved pixels having different pixel- and readout pitches, MCM-D structures, and the use of diamond as a sensor. Hybrid pixels in which radiation quanta are individually counted and summed over an exposure time have opened a new approach in radiology imaging, especially at low dose rates. Monolithic or semi-monolithic detectors, in which detector and readout ultimately are one entity, are currently being developed in various forms, largely driven by the needs for particle detection at future colliders. CMOS active pixel sensors using standard commercial technologies on low resistivity bulk and SOI pixels, a-Si:H, and DEPFET-pixels, which try to maintain high bulk resistivity for charge collection, constitute the different efforts to monolithic detectors which are presently being carried out.
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References

[1] The ALICE collaboration. ALICE Technical Design Report of the Inner Tracker System. CERN/LHCC/99-12, 1999.

[2] P. Riedler et al. First results from the ALICE silicon pixel detector prototype. *Nucl. Inst. and Meth.*, A501:111–118, 2003.

[3] The ATLAS collaboration. Technical Design Report of the ATLAS Pixel Detector. CERN/LHCC/98-13, 1998.

[4] C. Gemme at al. ATLAS Pixel Collaboration. The ATLAS pixel detector. *Nucl. Inst. and Meth.*, A501:87–92, 2003.

[5] The CMS collaboration. CMS Tracker Technical Design Report. CERN/LHCC/98-6, 1998.

[6] W. Erdmann. The CMS pixel detector. *Nucl. Inst. and Meth.*, A447:178–183, 2002.

[7] T. Gys. The pixel hybrid photon detectors for the LHCb-RICH project. *Nucl. Inst. and Meth.*, A465:240–246, 2001.

[8] S. Kwan. The BTEV Pixel and Microstrip Detectors. *Nucl. Inst. and Meth.*, A511:48–51, 2003.

[9] A. Baldit, J. Castor, A. Devaux, B. Espagnon, P. Force, et al. ALICE Technical Design Report of the Inner Tracker System. CERN-SPSC-2000-010, 2002.

[10] E. Radermacher. First results on the na60 pixel telescope in in-in collisions. In *IEEE2003 Nuclear Science Symposium*, Portland, Oct 2003. submitted to IEEE Trans. Nucl. Sci. (2004).

[11] G. Lindström et al. ROSE Collaboration. Radiation damage in silicon detectors. *Nucl. Inst. and Meth.*, A512:92–95, 2003.

[12] M. S. Alam et al. The ATLAS Silicon Pixel Sensors. *Nucl. Inst. and Meth.*, A456:217–231, 2001.

[13] L. Blanquart et al. FE-I1: A Front-end Readout Chip Designed in a Commercial 0.25µm process for the ATLAS pixel detector at LHC. *IEEE Trans. Nucl. Sci.*, vol. 51, no. 4:1358–1364, 2004.
[14] C. Gemme et al. Study of Indium bumping for the ATLAS pixel detector. *Nucl. Inst. and Meth.*, A465:200–203, 2001.

[15] A.M. Fiorello. ATLAS bump bonding process. In *Pixel 2000 Conference, Genoa, Italy*, June 2000.

[16] R. Horisberger (PSI Zurich). Private communication.

[17] P. Fischer. An area efficient 128 channel counter chip. *Nucl. Inst. and Meth.*, A378:287–300, 1996.

[18] H. Graafsma. Detector needs at current and future synchrotron sources. In *IEEE2004 Medical Imaging Conference*, Portland, USA, Oct. 2003.

[19] E.M. Westbrook. Pixels and Proteins: Better detectors for biological crystallography. In *IEEE Trans. Nucl. Sci.*, Portland, USA, Oct. 2003.

[20] P. Fischer, A. Helmich, M. Lindner, N. Wermes, and L. Blanquart. A photon counting chip with energy windowing. *IEEE Trans. Nucl. Sci.*, 47(3):881–884, 2000.

[21] P. Fischer H. Krüger, M. Lindner, L. Blanquart and N. Wermes. Medical X-ray imaging with energy windowing. *Nucl. Inst. and Meth.*, A465:229–234, 2000.

[22] X. Llopart, M. Campbell, R. Dinapoli, D. SanSegundo, and E. Pernigotti. MEDIPiX2: A 64-k pixel readout chip with 55μm² elements working in single photon counting mode. *IEEE Trans. Nucl. Sci.*, 49(5):2279–2283, 2002.

[23] G. Mettivier, M.C. Montesi, and P. Russo. Autoradiography with a MEDIPiX2 hybrid silicon pixel detector. In *IEEE2004 Medical Imaging Conference*, Portland, USA, Oct. 2003.

[24] M. Löcker et al. Single photon counting X-ray imaging with Si and CdTe single chip pixel detectors and multichip pixel modules. *IEEE Trans. Nucl. Sci.*, vol. 51, no. 4:1717–1723, 2004.

[25] MEDIPiX Collaboration, S.R. Amendolia, et al. Semiconductor pixel detectors for digital mammography. *Nucl. Inst. and Meth.*, A509:283–289, 2003.

[26] P. Fischer, J. Hausmann, A. Helmich, M. Lindner, N. Wermes, and L. Blanquart. A counting pixel readout chip and sensor system for X-ray imaging. *IEEE Trans. Nucl. Sci.*, 46(4):1070–1074, 1999.

[27] P. Fischer, P. Fischer, M. Kouda, H. Krüger, M. Lindner, G. Sato, T. Takahashi, S. Watanabe, and N. Wermes. A counting CdTe pixel detector for hard X-ray and gamma-ray imaging. *IEEE Trans. Nucl. Sci.*, 48(4):2401–2404, 2001.

[28] N. Jung et al. Dynamic X-ray imaging based on an amorphous silicon thin-film array. In *SPIE 3336*, 396–407, 1998.

[29] P.R. Granfors et al. Performance of a flat panel cardiac detector. In *SPIE 4320*, 77–86, 2001.
[30] M. Choquette et al. Performance of a real-time selenium based detector for fluoroscopy. In SPIE 4320, 501–508, 2001.

[31] F. Busse et al. Design and performance of a high-quality cardiac flat detector. In SPIE 4682, 819–827, 2002.

[32] O. Tousignant et al. Progress report on the performance of real-time selenium flat-panel detectors for direct X-ray imaging. In SPIE 4682 (2002) 503-510, 2002.

[33] P. Delpierre et al. X-ray pixel detector for crystallography. IEEE Trans. Nucl. Sci., 48(4):987–991, 2001.

[34] P. Delpierre et al. Large surface X-ray pixel detector. IEEE Trans. Nucl. Sci.

[35] C. Brönnimann et al. A pixel detector for the protein crystallography beamline at the SLS. Journal of Syn. Rad., 7:301, 2000.

[36] E. Eikenberry et al. The PILATUS X-ray detector. In IEEE2004 Conference on Room Temperature Sensitive Devices, Portland, USA, Oct. 2003.

[37] C. Kenney, S. Parker, J. Segal, and C. Storment. Silicon detectors with 3-D electrode arrays: fabrication and initial test results. IEEE Trans. Nucl. Sci., vol.48, no.4:1224–1236, 1999.

[38] S.I. Parker et al. Session and talks at this conference (STD5 Hiroshima), 2004.

[39] W. Adam et al. Development of Diamond Tracking Detectors for High Luminosity Experiments at the LHC. Nucl. Inst. and Meth., A447:244, 2000.

[40] M. Keil et al. New results on diamond pixel sensors using ATLAS frontend electronics. Nucl. Inst. and Meth., A511:153–159, 2003.

[41] T. Lari, A. Oh, N. Wermes, H. Kagan, M. Keil, and W. Trischuk. Characterization and modeling of non-uniform charge collection in cvd diamond pixel detectors. Nucl. Inst. and Meth., 2004. e-Print Archive: physics/0409120, accepted for publication in Nucl. Inst. Meth. A (2004).

[42] H. Kagan. Recent Advances in Diamond Detector Development. In 5th Int. Symposium on Development and Application of Semiconductor Tracking Detectors, Hiroshima, Japan, June 2004. these proceedings.

[43] W. Kucewicz, G. Deptuch, A. Zalewska, M. Battaglia, K. Osterberg, et al. Capacitively coupled active pixel sensors with analog readout for future e^+e^- colliders. Acta Phys. Polon., B30:2075–2083, 1999.

[44] J. Wolf, P. Gerlach, M. Töpper, K. Scherpinski, D. Petter, C. Kallmayer, O. Basken, C. Grah, K.H. Becks, N. Wermes, O. Ehrmann, H. Reichland, et al. High density pixel detector module using flip chip and thin film technology. In SPIE Conference, Denver, USA, 2000. SPIE Vol. 4217, (2000) 553-556.

[45] T. Flick, K.H. Becks, P. Gerlach, C. Grah, P. Mättig, and T. Rohe. Studies on MCM-D pixel-detector-modules. Nucl. Phys. B proc. suppl., 125:85–89, 2003.
[46] T. Behnke, S. Bertolucci, R.-D. Heuer, and R. Settles (eds.). TESLA Technical Design Report. *Report DESY-01-011*, Vol. IV, 2001.

[47] W. Snoeys, J. Plummer, S. Parker, and C. Kenney. A new integrated pixel detector for high energy physics. *IEEE Trans. Nucl. Sci.*, vol.39:1263–1269, 1992.

[48] G. Meynants, B. Dierickx, and D. Scheffer. CMOS active pixel image sensor with CCD performance. *Proceedings SPIE - Int. Soc., Opt. Eng. (USA)*, 3410:68–76, 9., 1998.

[49] R. Turchetta, J.D. Berst, B. Casadei, G. Claus, C. Colledani, W. Dulinski, Y. Hu, D. Husson, J.-P. Le-Normand, J.L. Riester, G. Deptuch, U. Goerlach, S. Higueret, and M. Winter. A monolithic active pixel sensor for charged particle tracking and imaging using standard VLSI CMOS technology. *Nucl. Inst. and Meth.*, A458:677–689, 2001.

[50] G. Claus, C. Colledani, W. Dulinski, D. Husson, R. Turchetta, J.L. Riester, D. Deptuch, G. Orazi, and M. Winter. Particle tracking using CMOS monolithic active pixel sensor. *Nucl. Inst. and Meth.*, A465:120–124, 2001.

[51] G. Deptuch, W. Dulinski, Y. Gornushkin, C. Hu-Guo, and I. Valin. Monolithic active pixel sensor with in-pixel amplification and double sampling operation. *Nucl. Inst. and Meth.*, A512:299–309, 2003.

[52] G. Deptuch et al. Monolithic active pixel sensor with in-pixel double sampling and column-level discrimination. In *IEEE Nuclear Science Symposium 2003*, Portland, USA, Oct. 2003. submitted for publication in IEEE-TNS (2004).

[53] R. Turchetta. Monolithic active pixel sensors (MAPS) for particle physics and space science. In *Proc. VERTEX 2003*, Lake Windermere, UK, Sept. 2003.

[54] H. Matis, F. Bieser, S. Kleinfelder, G. Rai, F. Retiere, H. Ritter, K. Singh, S. Wurzel, H. Wiemann, and E. Yamamoto. Charged particle detection using a CMOS active pixel sensor. *IEEE Trans. Nucl. Sci.*, 50:1020–1025, 2003.

[55] G. Varner et al. Development of a Super B-Factory Monolithic Active Pixel Detector - the Continuous Acquisition Pixel (CAP) Prototypes. In 5th *Int. Symposium on Development and Application of Semiconductor Tracking Detectors*, Hiroshima, Japan, June 2004. these proceedings.

[56] W. Dulinski, D. Berst, F. Cannillo, G. Claus, C. Colledani, et al. CMOS monolithic active pixel sensors for high resolution particle tracking and ionizing radiation imaging. In *Proc. Frontier Detectors for Frontier Physics 2003*, Elba, May 2003.

[57] A. Gay. High resolution CMOS sensors for a vertex detector at the linear collider. In *Proc. Vertex 2003 Conference*, Lake Windermere, UK, September 2003.

[58] S. Kleinfelder et al. Novel integrated CMOS pixel structures for vertex detectors. In *IEEE Nuclear Science Symposium 2003*, Portland, USA, Oct. 2003. Conference Record IEEE, Vol.1, 2004, lii+3759 p.335-9 Vol.1, 9.
[59] J. Marczewski et al. SOI active pixel detectors of ionizing radiation - technology and design development. *IEEE Trans. Nucl. Sci.*

[60] W. Kucewicz. Development of monolithic active pixel detector in soi technology. In *5th Int. Symposium on Development and Application of Semiconductor Tracking Detectors*, Hiroshima, Japan, June 2004. these proceedings.

[61] M. Amati, M. Baranski, A. Bulgheroni, M. Caccia, K. Domanski, et al. Hybrid Active Pixel Sensors and SOI inspired option. *Nucl. Inst. and Meth.*, A511:265–270, 2003.

[62] J.A. Theil et al. a-Si:H photodiode technology for advanced CMOS active pixel sensor imagers. In *19th Intl. Conf. on Amorphous Materials and Semiconductors*, Nice, August 2001.

[63] P. Jarron. Deposition of amorphous silicon above integrated circuits. In *19th Intl. Conf. on Advanced Detectors*, Elba, May 2003.

[64] J. Kemmer and G. Lutz. New semiconductor detector concepts. *Nucl. Inst. and Meth.*, A253:356–377, 1987.

[65] E. Gatti and P. Rehak. Semiconductor drift chamber - an application of a novel charge transport scheme. *Nucl. Inst. and Meth.*, A225:608, 1984.

[66] J. Ulrici, P. Fischer, P. Klein, G. Lutz, W. Neeser, R. Richter, L. Strüder, M. Trimpl, and N. Wermes. Imaging performance of a DEPFET bioscope system in tritium autoradiography. *submitted for publication in Nucl. Inst. and Meth. A*, 2004.

[67] P. Fischer, M. Schuchtemer, M. Trimpl, J. Ulrici, N. Wermes, L. Andricek, G. Lutz, and R. Richter. Desy Linear Collider note. LC-DET-2002-004, 2002.

[68] N. Wermes et al. New results on DEPFET pixel detectors for radiation imaging and high energy particle detection. In *IEEE Trans. Nucl. Sci.*, Portland, USA, Oct. 2003. accepted by IEEE Trans. Nucl. Sci (2004).

[69] P. Holl, P. Fischer, R. Hartmann, G. Hasinger, J. Kollmer, et al. Active pixel sensor for X-ray imaging spectrometers. In *SPIE Int. Soc. Opt. Eng, vol 4851 (2003)* 770-778, San Diego, 2003.

[70] M. Trimpl, L. Andricek, P. Fischer, G. Lutz, R.H. Richter, L. Strüder, J. Ulrici, N. Wermes, and M. Trimpl. A fast readout using switched current techniques for a DEPFET-pixel vertex detector at tesla. *Nucl. Inst. and Meth.*, A511:257–264, 2003.

[71] L. Andricek, G. Lutz, M. Reiche, and R.H. Richter. Processing of ultra thin silicon sensors for future linear collider experiments. *IEEE Trans. Nucl. Sci.*, vol.51, no.3:1117–1120, 2004.