Orthostatic Intolerance Is Independent of the Degree of Autonomic Cardiovascular Adaptation after 60 Days of Head-Down Bed Rest

Jiexin Liu, Yongzhi Li, Bart Verheyden, Zhanghuang Chen, Jingyu Wang, Yinghui Li, André E. Aubert, and Ming Yuan

1 Department of Cardiology, Beijing Friendship Hospital, China Capital Medical University, Beijing 100050, China
2 Department of Cardiology, University Hospital Gasthuisberg, KU Leuven, 3000 Leuven, Belgium
3 State Key Laboratory of Space Medicine Fundamentals and Application, China Astronaut Research and Training Center, Beijing 100094, China

Correspondence should be addressed to André E. Aubert; andre.aubert@med.kuleuven.be and Ming Yuan; yuanming7@hotmail.com

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Spaceflight and head-down bed rest (HDBR) can induce the orthostatic intolerance (OI); the mechanisms remain to be clarified. The aim of this study was to determine whether or not OI after HDBR relates to the degree of autonomic cardiovascular adaptation. Fourteen volunteers were enrolled for 60 days of HDBR. A head-up tilt test (HUTT) was performed before and after HDBR. Our data revealed that, in all nonfainters, there was a progressive increase in heart rate over the course of HDBR, which remained higher until 12 days of recovery. The mean arterial pressure gradually increased until day 56 of HDBR and returned to baseline after 12 days of recovery. Respiratory sinus arrhythmia and baroreflex sensitivity decreased during HDBR and remained suppressed until 12 days of recovery. Low-frequency power of systolic arterial pressure increased during HDBR and remained elevated during recovery. Three subjects fainted during the HUTT after HDBR, in which systemic vascular resistance did not increase and remained lower until syncope. None of the circulatory patterns significantly differed between the fainters and the nonfainters at any time point. In conclusion, our data indicate that the impaired orthostatic tolerance after HDBR could not be distinguished by estimation of normal hemodynamic and/or neurocardiac data.

1. Introduction

The lack of gravitational stress during spaceflight is associated with many adaptations in cardiovascular structure as well as neurohumoral control circuits [1–7]. One important negative manifestation is postspaceflight orthostatic intolerance (OI) [8], which is a current operational problem for many astronauts. Due to limitations related to human spaceflight, such as high cost, limited access, small number of subjects, and limited crew time, head-down bed rest (HDBR) has been used to investigate the physiologic effects of spaceflight as a microgravity simulation model [9].

Cardiovascular adaptations to HDBR have been studied over the past 20 years. During the first hours of HDBR, body fluid shifts from the lower to the upper part of the body, resulting in a transient increase in thoracic plasma volume [10, 11]. This expanded plasma volume simulates central volume carotid, aortic, and cardiac receptors, induces an increase in diuresis and natriuresis as well as a decrease in plasma volume, and restores central blood volume to baseline levels after a couple of days [12–14]. Moreover, it has been reported that HDBR leads to a decrease in vagal control of the cardiac system and an increase in vasomotor sympathetic tone as well as a decrease in baroreflex sensitivity (BRS) [12, 15–18]. Similar to what occurs after spaceflight, these adaptations facilitate the occurrence of postural tachycardia with a variable degree of OI after HDBR [9].
A number of studies have focused on the mechanism of postspaceflight or post-HDBR orthostatic intolerance. Most of the studies were conducted with postural stress, such as the head-up tilt test (HUTT). Nevertheless, whether or not OI relates to the degree of autonomic cardiovascular adaptations is uncertain. If it does not relate to the degree of autonomic cardiovascular adaptations, what are the determinants of this phenomenon? In addition, another attractive and practical question is to determine who will have poor orthostatic tolerance after microgravity or microgravity simulation; that is, can postspaceflight or post-HDBR OI be predicted by the responses to a normal HUTT?

The purpose of this study was to test the hypothesis that fainters (subjects with a positive orthostatic stress test after HDBR) will have lower vagal cardiac control, a lower arterial baroreflex, and higher sympathetic activity after prolonged HDBR compared to nonfainters (subjects with a negative orthostatic stress test after HDBR) by detecting the differences in hemodynamic and cardiovascular autonomic control as well as arterial baroreflex function in fainters and nonfainters.

2. Materials and Methods

2.1. Study Population. Fourteen healthy male volunteers of Asian descent (age, 30 ± 1 years; height, 169 ± 1 cm; weight, 62 ± 1 kg) were enrolled in this 60-day HDBR study. All subjects spent 90 days in the Bed Rest Study Lab in the China Astronaut Research and Training Center (ACC; Beijing, China) as follows: 15-day pretest period for Lab in the China Astronaut Research and Training Center study. All subjects spent 90 days in the Bed Rest Study weight, 62±1 kg) were enrolled in this 60-day HDBR protocol started with the subjects resting quietly in the supine (before and after HDBR) or in head-down position (during HDBR) with comfortable, uncontrolled respirations for 10 min as a baseline recording. Then, the subjects were instructed to pace their breathing to an audio stimulus. Controlled breathing was held for 3 min, during which respiratory sequences were evenly spaced in time at a preset rate of 12 breaths min⁻¹ or 0.2 Hz [19].

A HUTT was performed twice at 75° before (at BDC 4 day) and after bed rest (R + 0). After a period of 10 min in the supine position, volunteers were tilted to the 75° head-up tilt position for a maximum duration of 20 min. Immediately after fainting or completing the entire tilt duration, that is, 20 min, the subjects were tilted back to the supine position for a 10 min recovery.

During the HUTT, syncope was defined as the loss of consciousness accompanied by severe hypotension and/or bradycardia (systolic blood pressure <70 mmHg; heart rate (HR) decrease >15 beats/min). At the time of impending syncope, typical symptoms and signs included lightheadedness, nausea, blurred vision, pallor, and sweating.

Volunteers were regarded as nonfainters or fainters according to the HUTT results after 60 days of HDBR. The nonfainters were defined as subjects who completed HUTT without fainting; in contrast, the fainters were defined as subjects who had the test aborted due to syncope.

2.3. Data Acquisition and Analysis. Noninvasive beat-to-beat blood pressure (BP) was measured with an infrared finger photoplethysmograph (Finometer Blood Pressure Monitor; TNO-TPD Biomedical Instrumentation, Amsterdam, Netherlands). The hand was held at heart level to avoid hydrostatic pressure differences. The measured signal was analog-to-digital converted at 1000 Hz and stored on a hard disk for offline analysis. Systolic arterial pressure and diastolic arterial pressure were derived from the arterial pressure waveform. Mean arterial pressure (MAP) was the true integral of the arterial pressure wave over one beat divided by the corresponding beat interval. Pulse pressure (PP) was defined as the difference between systolic pressure and diastolic pressure. HR was computed from ECG recording and expressed as beats per minute.

During the 3 min paced breathing protocol, beat-to-beat SAP and the RR interval (RRI) time series were constructed for frequency analysis. First, two linear filters (SD filter and 20% mean values) were applied to correct for data points outside a limit interval [20]. The resulting beat-to-beat hemodynamic time series was interpolated using a cubic-spline approximation and resampled at 2 Hz to construct equidistant time series. A sliding window of 128 sec (256 samples) was applied with 16 sec increments. This process resulted in four segments of data in each time series. The DC component was removed by subtracting the mean value, and a Hanning window was applied. A nonparametric
“run test” of means and mean square values was used to validate the stationarity of data within 5% of the confidence limits [20]. In the resulting time windows, power spectral density was averaged using fast Fourier transformation. The spectral resolution for all estimates equaled 0.0078 Hz. Respiratory powers were expressed as the area under the spectrum from 0.18 to 0.22 Hz and used as a marker of respiratory sinus arrhythmia (RSA). A second spontaneous rhythm occurring over an approximate 10 sec cycle and resulting in a low-frequency band (0.04–0.15 Hz) was obtained as well for SAP variability [21]. Power spectral units for RRI and SAP fluctuations were squared amplitudes.

During the 10 min baseline recording time domain analysis of spontaneous BRS was performed using the cross-correlation method [22]. In a 10 sec window, the correlation and regression slope between SAP and RRI were computed. Delays of 0–5 sec increments in RRI were computed, and the delay with the highest positive coefficient of correlation was selected (tau). The slope between SAP and RRI was recorded and compared. The slope between SAP and RRI was computed.

Correlation method [22]. In a 10 sec window, the correlation analysis of spontaneous BRS was performed using the cross-correlation method. The number of significant BRS estimates was also calculated and expressed per minute. Thus, the following three complementary aspects of arterial baroreflex function were assessed: (1) BRS, which provides qualitative information; (2) number of BRS estimates, which provides quantitative information; and (3) tau, which provides temporal information on cardiac baroreflex control.

Orthostatic intolerance before and after HDBR was tested with HUTT. Continuous changes in stroke volume (SV) were estimated by modeling flow from the arterial pressure waveform (Modelflow; TNO Biomedical Instrumentation) expressed in mL [23]. Cardiac output (CO; expressed in L/min) was the product of the estimated SV and HR, and systemic vascular resistance (SVR; expressed in mmHg/s/mL [also referred to as medical units or MUs]) was the MAP at the heart level divided by the computed CO. The Modelflow method computes aortic flow from the finger arterial pressure by simulating a nonlinear model of the aortic input impedance [23]. This pulse wave analysis method corrects for individual differences in age, gender, height, and weight [24], thus permitting group average data to be examined accurately in subjects without structural or functional heart disease [25, 26]. Previous head-up tilt experiments have demonstrated good agreement between Modelflow and standard CO estimates, such as inert gas rebreathing [27], thermodilution [28], and Doppler ultrasound [29]. Under the adverse circumstances of very low arterial BPs, Modelflow and standard CO estimates, such as inert gas rebreathing [27], thermodilution [28], and Doppler ultrasound [29]. Under the adverse circumstances of very low arterial BPs, Modelflow computations have also been shown to be accurate [30].

### 2.4. Statistical Analysis

Statistical analysis was performed with SPSS (version 13.0 for Windows; Scientific Packages for Social Sciences, Inc., Chicago, IL, USA) and Prism 5.0 (GraphPad, San Diego, CA, USA). Data are given as the median (25, 75 percentiles) or mean ± SD. Spectral data were logarithmically transformed if needed to approximate normal distributions. The evolutions of hemodynamic and spectral and baroreflex indices before, during, and after HDBR were analyzed across conditions using one-way repeated measures ANOVA if data passed the D’Agostino and Pearson omnibus normality test. Simple contrast analysis was conducted to evaluate changes at each time point as compared to baseline by Bonferroni’s multiple comparison test. If any data didn’t pass the normality test, they were analyzed by Kruskal-Wallis test and then performed Dunn’s test for multiple comparison. During the HUTT before and after HDBR, hemodynamic parameters in the nonfainters were evaluated and compared with two-way repeated measures ANOVA. P values < 0.05 were considered statistically significant.

### 3. Results

All of the subjects completed the study. No volunteer fainted during the HUTT before HDBR; three volunteers were regarded as fainters because of the positive HUTT after HDBR, and the others (n = 11) were regarded as nonfainters. Before HDBR, there were no differences in age, weight, and height between the nonfainters (age, 30 ± 4 years; weight, 60 ± 4 kg; height, 169 ± 4 cm) and the fainters ((A): age, 27 years; weight, 63 kg; height, 173 cm; (B): age, 29 years; weight, 58 kg; height, 170 cm; (C): age, 39 years; weight, 66 kg; height, 173 cm). After HDBR, the weight increased in the two groups as follows: nonfainters, 63 ± 5 kg (P = 0.008, compared to before HDBR), and fainters ((A), 67 kg; (B), 64 kg, and (C), 70 kg).

#### 3.1. Evolutions in Circulatory Control

Figure 1 shows the changes in HR, MAP, and respiratory frequency before, during, and after HDBR. On average, in all nonfainters (n = 11), there was a progressive rise in HR until day 56 of HDT (from 69 beats/min [61, 77 beats/min] before HDBR to 73 beats/min [69, 81 beats/min] at HDT41, P < 0.01). The HR remained significantly higher until day 12 of recovery. The MAP increased gradually until day 56 of HDT (from 80 mmHg [75, 83 mmHg] before HDBR to 91 mmHg [86, 99 mmHg] at HDT56, P < 0.001) and then returned to baseline after 12 days of recovery. The respiration frequency decreased during HDBR (from 16 min−1 [14, 18 min−1] before HDBR to 14 min−1 [12, 17 min−1] at HDT56, P < 0.05) and returned to baseline during the recovery. Evolutions of BRS, the number of baroreflex estimates, and tau before, during, and after HDBR are shown in Figure 2. In all nonfainters, BRS significantly decreased at HDT56 (from 12.7 ms/mmHg [9.9, 23.6 ms/mmHg] before HDBR to 10.1 ms/mmHg [7.5, 13.1 ms/mmHg] at HDT41, P = 0.0241) and remained suppressed until R12. The number of baroreflex estimates per min decreased on HDT2 (from 11 min−1 [8, 14 min−1] before HDBR to 9.0 min−1 [7, 11 min−1] at HDT2, P = 0.033) and then gradually recovered to baseline after 56 days of HDBR. Tau remained stable during the HDBR and during recovery. The alterations in RSA and low-frequency power of SAP are shown in Figure 3. In nonfainters, RSA fluctuated during HDBR and returned to baseline during the recovery. Low-frequency power of SAP significantly increased on HDT2 (from 1.592 mmHg2 [1.148, 1.705 mmHg2] before HDBR to 2.25 mmHg2 [1.939, 2.537 mmHg2] at HDT2, P = 0.0095) and showed a tendency to be increased until HDT56. A further increase in the low-frequency power of SAP was observed.
during the recovery (1.948 mmHg² [1.519, 2.723 mmHg²] at day R6, \( P = 0.015 \) and 2.089 mmHg² [1.711, 2.629 mmHg²] at day R12, \( P = 0.0427 \) compared to data from controlled breathing before HDBR). None of the circulatory adaptations to HDBR significantly differed between the fainters and the nonfainters at any time point (Figures 1–3).

3.2. Orthostatic Circulatory Control. In the positive HUTT (\( n = 3 \)), the time range from the start of tilt to the syncopal episode was from 6.8 to 12.0 min. The changes in HR, SAP,
and DAP of the three fainters 5 min before and 4 min after the syncopal episodes during HUTT are shown in Figure 4. According to the VASIS classification of the European Society of Cardiology (ESC) [31], all fainters were of the mixed type (a fall in BP comes first, followed by a decrease in HR, without marked bradycardia or asystole). The drops in HR and BP started 1-2 minutes before the syncopal episode; the BP recovered quickly 2 min after tilting back to the supine position.

Hemodynamic responses to tilting before and after HDBR are shown in Figure 5. Before HDBR, the responses to tilting were similar in all parameters in all subjects not only during the first 2 min immediately after the tilt but also during the last 2 min at the end of tilt testing. HR, MAP, and SVR significantly increased after tilting and remained higher until the end of tilting; SV and CO significantly decreased after tilting and remained lower until the end of HUTT. After HDBR, in the nonfainters (n = 11) at baseline in the supine position, hemodynamic parameters remained at the same level compared to pre-HDBR, except that there was a significant rise in MAP (from 84 mmHg before HDBR to 97 mmHg after HDBR, P = 0.003). Immediately after tilting, the HR and MAP significantly increased. These increases were more pronounced after HDBR (P < 0.001 in both HR and MAP); SV markedly decreased compared with a larger increase in SVR. Compared to the HUTT before HDBR, the decrease in SV was larger (P = 0.022) and the increase in SVR also showed a tendency to be increased (P = 0.058). CO significantly decreased similar to the previous one. At the end of tilt testing, HR increased further (P = 0.024); the MAP remained at the higher level (P = 0.127) and the SVR tended to increase slightly (P = 0.331), compensated by a further decrease in SV (P = 0.053) simultaneously. CO did not change compared to the beginning of tilting. In the three fainters, immediately after tilting, HR increased more in the two fainters compared to the nonfainters, but the MAP did not increase. The SV was significantly decreased in all fainters and, due to the larger increase in HR, CO seemed to be higher compared to the nonfainters. SVR was unchanged after tilting. Before a syncopal episode, SVR remained at a low level in all fainters. A steeper drop in the HR, MAP, SV, and CO was observed in two of the three fainters (Figure 5).

4. Discussion

In the current study cardiovascular and respiratory control was evaluated in 14 healthy volunteers before, during, and after a 60-day HDBR eliciting cardiovascular adaptations. This study focused on the possible influence of hemodynamic parameters altering autonomic cardiovascular control after HDBR. The main findings of the present investigation were twofold. First, the evolution in hemodynamic and respiratory parameters during long-term HDBR was similar in fainters and nonfainters; that is, OI after microgravity simulation was not predicted by normal estimation of hemodynamic and/or neurocardiac data. Second, in agreement with our previous findings in vasovagal syncope patients [32,33], we found that prior to syncope there was a steep fall in CO in all fainters that was insufficiently compensated for by SVR.

During the past 20 years, HDBR has proven to be useful as a simulation model for space physiology studies on the ground. A number of previous studies have focused on cardiovascular regulation of the autonomic nervous system in bed rest studies. Most studies have reported a decrease in HRV and parasympathetic indices [16–18], implying a chronic cardiovascular adaptation to HDBR. In agreement with the European Space Agency, French Space Agency, and National Space Development Agency of Japan (ESA/CNES/NASDA) clinical report, which found a progressive increase in resting HR in the second half of the study during a 90-day HDBR [9], we also found that HR was significantly increased after HDT41; specifically, respiratory sinus arrhythmia decreased, while BP and the low-frequency power of BPV continuously increased. These results are in agreement with Kamiya et al. [34] who showed an increase in vasomotor sympathetic tone, as determined from muscle
sympathetic nerve activity on the tibial nerve with long-term HDBR (60 and 120 days). This suggests that long-term HDBR results in a reduction in vagal cardiac control and a rise in sympathetic activity. Moreover, in agreement with previous studies showing that the spontaneous baroreflex slope decreased during and/or after HDBR [12, 16–18, 35], we observed a gradual reduced BRS slope during HDBR, suggesting that the cardiac baroreflex mechanism is disturbed after a prolonged period of bed rest. In addition, we also found a transient decrease in the number of baroreflex estimates at the beginning of HDBR. It is likely that the decrease in the quantity of BRS is consistent with the previously reported transient increase in thoracic blood volume [10, 11] due to the initial fluid shift from the lower part to the upper part of the body, while the decrease in the quality of BRS is coincident with the previously reported subsequent decrease in plasma volume and the restoration of central blood volume to baseline levels in the latter part of bed rest [12–14]. This finding implies that the quantitative and qualitative changes in BRS are elicited by reversed hemodynamics.

Furthermore, in agreement with previous findings during spaceflight [19, 36], our study showed a decrease in respiration frequency during HDBR. Although this special phenomenon is difficult to explain with our current knowledge, it might be speculated that a decrease in respiration frequency might be related to a reduction in lung volume [37], tidal volume, pulmonary ventilation, and metabolic rate [36], which may be a physiologic response to reduced metabolic demand [19]; however, further studies are needed.

It has been shown that exposure to actual or simulated microgravity alters physiologic adaptive mechanisms and reduces exercise capacity and orthostatic tolerance [8, 38–40]. Head-up tilt testing was performed as orthostatic stress in this study. With our current experimental protocol, orthostatic tolerance was reduced in three volunteers after HDBR. Based on our existing data, we rejected our hypothesis that the fainters would have lower vagal cardiac control, a lower arterial baroreflex, and higher sympathetic activity after prolonged HDBR. In fact, we could not distinguish the hemodynamic and autonomic differences between the fainters and nonfainters during and after HDBR with our definition of fainting by HUTT. Thus, we infer that fainting after bed rest does not relate to the degree of neural cardiovascular changes induced by HDBR. A number of previous studies have used the response to an orthostatic stress test to evaluate mechanisms of OI; however, our data suggest that this may not be a good strategy for investigating the neural contribution to OI because the individual response.

**Figure 4:** Heart rate (HR), systolic blood pressure (SBP), and diastolic arterial pressure (DAP) of 3 fainters (a, b, and c) 5 minutes before and 4 minutes after syncope during the positive HUTT after HDBR. Heart rate and blood pressure (BP) decreased together before the syncope episode.
Figure 5: Changes in estimated heart rate (HR), mean arterial pressure (MAP), stroke volume (SV), cardiac output (CO), and systemic vascular resistance (SVR) from supine until the end of head-up tilt testing. Values in the supine position during the first and last 2 minutes of the tilt are presented as averages at 20-second intervals. In the nonfainters (n = 11), phase indicates the different moment during HUTT, and session includes two parts (pre-HDBR and post-HDBR).
to an orthostatic stress test does not necessarily appear to distinguish between subjects who are deconditioned and those who are not.

Unexpectedly, we found only three of 14 fainters, whereas at least seven of 14 would be expected as fainters according to the literature (99 of 172 resulting from 12 male-only studies [references in the review by Pavy-Le Traon et al. [9]]). A possible reason might be the daily use of the bathroom by the subjects; however, daily toilet visits cannot be viewed as a specific countermeasure, as the behavior of all parameters was in agreement with the results from most studies [12, 16–18, 34, 35]. Another possible reason might be attributed to water intake, which has a significant influence on OI. Unfortunately, the daily water intake was not controlled in this study; thus we cannot evaluate whether or not the low occurrence rate of OI was due to the uncontrolled fluid intake. Moreover, an increase in weight for the fainters can also be hypothesized, although no physiologic correlation has been shown in the literature.

In the three fainters, the tilt-induced syncope episode appears to be cardiac output-mediated, with a rapid drop in HR and SV, which begins several minutes prior to the occurrence of syncope, but without a marked fall in SVR. These cardiovascular responses are precisely similar to what we found in the vasovagal syncope patients [32, 41]; however, two major differences existed between the fainters and the nonfainters in hemodynamic changes during orthostatic stress. First, the MAP was higher in the nonfainters than in the fainters at the beginning of HUTT and was maintained until the end of HUTT. Second, the nonfainters had a similarly increased SVR response to tilting before and after bed rest as well as a further increase at the end of HUTT after bed rest; however, in the fainters, SVR was lower from the beginning of HUTT until the occurrence of syncope. A logical explanation for this phenomenon might be the fact that HDBR reduced vasomotor modulation in the fainters, resulting in an impaired vasoconstriction response to the increase in postural change, leading to a diminished cardiovascular reserve. In agreement with our results, but using a different study approach, Buckey et al. [8] showed that nine of 14 astronauts could not complete a 10 min postflight stand test that all were able to complete before flight, suggesting that the subjects who were able to complete the test had a higher vasoconstrictor response and maintained SVR, while the fainters did not. In a study of Butler et al. [40], it was speculated that the cause of the impaired orthostatic tolerance is a decreased tone in venous capacitance vessels. Using ultrasonography, Arbeille et al. [42] also demonstrated that the fainters showed a lack of leg vasoconstriction and higher calf vein distensibility during HUTT after a 60-day HDBR. Therefore, we suggest that the impaired vasomotor modulation might be a main reason for OI after spaceflight or HDBR. A recent study involving vasovagal syncope by Verheyden et al. [32] provided circumstantial evidence of this outcome. It was documented that orthostatic tolerance can be improved by increasing the amount of vasoconstriction after 6 weeks of continued standing training, which increased the vasoconstrictor reserve in vasovagal syncope patients [32]; however, further studies are still needed.

The present results suggest that prolonged HDBR results in a decreased BRS, which is similar to postspaceflight. Fritsch et al. [43] observed a functionally relevant impairment in BRS after missions of 4–5 days in space and a reduction of BRS after missions of 8–14 days [44]. Cooke et al. [45] reported a reduced vagal baroreflex gain after a 9-month long duration space mission; however, we suggest that the similar decrease in BRS could be due to different mechanisms, such as immobilization and inactivity in HDBR and lack of gravity stimulation during space missions.

Unlike HDBR, HR has been reported to be stable [4, 19] or decreased [3, 45–47] during spaceflight. Additionally, it is likely that the differences between HDBR and real spaceflight are due to the great environment dissimilarity. A reasonable interpretation of these differences is the fact that as a ground-based simulation model HDBR cannot eliminate the influence of gravity. During bed rest, hydrostatic pressure at the heart level is higher than that during the supine position as well as during the standing position. This enhances the preload of the heart as well as the afterload acting as a feedback mechanism to increase the HR. During spaceflight, however, several studies have demonstrated a decrease in central venous pressure (CVP) [48, 49] together with increased cardiac chamber volumes [48]. Additionally, the strains during microgravity related to tissue compressions created by gravity disappear, leading to vasodilatation. This is facilitated by a decreased pleural pressure, which increases the distensibility of the pulmonary vessels and the vasculature [50]. As a result, the preload might increase, but the afterload probably decreases in space.

5. Conclusion

In all subjects, HDBR resulted in a decreased vagal cardiac control, an increased sympathetic activity, and a decreased arterial baroreflex. Post-HDBR orthostatic hypotension elicited by tilt testing is cardiac output-mediated, in which the lack of vasoconstriction also appears as an important inducement. The impaired orthostatic tolerance after HDBR could not be distinguished by estimation of normal hemodynamic and/or neurocardiac data.

Disclosure

The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the paper.

Conflict of Interests

All authors declare that there is no conflict of interests and agree with the contents of the paper.

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References

[1] A. R. Hargens and D. E. Watenpaugh, “Cardiovascular adaptation to spaceflight,” Medicine and Science in Sports and Exercise, vol. 28, no. 8, pp. 977–982, 1996.

[2] F. Beckers, B. Verheyden, J. Liu, and A. E. Aubert, “Cardiovascular autonomic control after short-duration spaceflights,” Acta Astronautica, vol. 65, no. 5–6, pp. 804–812, 2009.

[3] F. Beckers, B. Verheyden, and A. Aubert, “Evolution of heart rate variability before, during and after spaceflight,” Journal of Gravitational Physiology, vol. 10, pp. 107–108, 2003.

[4] B. Verheyden, J. X. Liu, F. Beckers, and A. E. Aubert, “Adaptation of heart rate and blood pressure to short and long duration space missions,” Respiratory Physiology and Neurobiology, vol. 169, no. 1, pp. S13–S16, 2009.

[5] M. B. Sides, J. Vernikos, V. A. Convertino et al., “The Bellagio report: cardiovascular risks of spaceflight: Implications for the future of space travel,” Aviation Space and Environmental Medicine, vol. 76, no. 9, pp. 877–895, 2005.

[6] R. J. White and M. Averner, “Humans in space,” Nature, vol. 409, no. 6823, pp. 1115–1118, 2001.

[7] L.-F. Zhang, “Vascular adaptation to microgravity: what have we learned?” Journal of Applied Physiology, vol. 91, no. 6, pp. 2415–2430, 2001.

[8] J. C. Buckey, L. D. Lane, B. D. Levine et al., “Orthostatic intolerance after spaceflight,” Journal of Applied Physiology, vol. 81, no. 1, pp. 7–18, 1996.

[9] A. Pavy-Le Traon, M. Heer, M. V. Narici, J. Rittweger, and J. Vernikos, “From space to Earth: advances in human physiology from 20 years of bed rest studies (1986–2006),” European Journal of Applied Physiology, vol. 101, no. 2, pp. 143–194, 2007.

[10] C. Gharib, G. Gauquelin, J. M. Pequignot, G. Geelen, C. A. Bizollon, and A. Guell, “Early hormonal effects of head-down tilt (-10 degrees) in humans,” Aviation, Space, and Environmental Medicine, vol. 59, no. 7, pp. 624–629, 1988.

[11] J. E. Greenleaf, “Physiology of fluid and electrolyte responses during inactivity: water immersion and bed rest,” Medicine & Science in Sports & Exercise, vol. 16, no. 1, pp. 20–25, 1984.

[12] D. Sieguado, J. O. Fortrat, A. Maillet, and et al., “Comparison of a 4-day confinement and head-down tilt on endocrine response and cardiovascular variability in humans,” European Journal of Applied Physiology and Occupational Physiology, vol. 73, no. 1-2, pp. 28–37, 1996.

[13] L. B. Johansen, C. Gharib, A.-M. Allevard et al., “Haematocrit, plasma volume and noradrenaline in humans during simulated weightlessness for 42 days;” Clinical Physiology, vol. 17, no. 2, pp. 203–210, 1997.

[14] S. Blanc, S. Normand, P. Ritz et al., “Energy and water metabolism, body composition, and hormonal changes induced by 42 days of enforced inactivity and simulated weightlessness;” Journal of Clinical Endocrinology and Metabolism, vol. 83, no. 12, pp. 4289–4297, 1998.

[15] H. W. J. Robbe, L. J. M. Mulder, H. Rueddel, W. A. Langewitz, J. B. P. Veldman, and G. Mulder, “Assessment of baroreceptor reflex sensitivity by means of spectral analysis,” Hypertension, vol. 10, no. 5, pp. 538–543, 1987.

[16] R. L. Hughson, Y. Yamamoto, A. P. Blaber et al., “Effect of 28-day head-down bed rest with countermeasures on heart rate variability during LBNP,” Aviation Space and Environmental Medicine, vol. 65, no. 4, pp. 293–300, 1994.

[17] A. Pavy-Le Traon, D. Sigaudo, P. Vasseur et al., “Cardiovascular responses to orthostatic tests after a 42-day head-down bedrest,” European Journal of Applied Physiology and Occupational Physiology, vol. 77, no. 1-2, pp. 50–59, 1998.

[18] K.-I. Iwasaki, R. Zhang, J. H. Zuckerman, J. A. Pawelczyk, and B. D. Levine, “Effect of head-down-tilt bed rest and hypovolemia on dynamic regulation of heart rate and blood pressure,” The American Journal of Physiology—Regulatory Integrative and Comparative Physiology, vol. 279, no. 6, pp. R2189–R2199, 2000.

[19] R. M. Baevsky, V. M. Baranov, I. L. Funtova et al., “Autonomic cardiovascular and respiratory control during prolonged spaceflights aboard the International Space Station,” Journal of Applied Physiology, vol. 103, no. 1, pp. 156–161, 2007.

[20] A. E. Aubert, D. Ramaekers, F. Beckers et al., “The analysis of heart rate variability in unrestrained rats. Validation of method and results,” Computer Methods and Programs in Biomedicine, vol. 60, no. 3, pp. 197–213, 1999.

[21] B. Verheyden, F. Beckers, K. Couckuyt, J. Liu, and A. E. Aubert, “Respiratory modulation of cardiovascular rhythms before and after short-duration human spaceflight,” Acta Physiologica, vol. 191, no. 4, pp. 297–308, 2007.

[22] B. E. Westerhof, J. Gisolf, W. J. Stok, K. H. Wesseling A, and J. M. Karemaker, “Time-domain cross-correlation baroreflex sensitivity: performance on the EUROBARAVAR data set,” Journal of Hypertension, vol. 22, no. 7, pp. 1371–1380, 2004.

[23] K. H. Wesseling, J. R. C. Jansen, J. J. Settels, and J. J. Schreuder, “Computation of aortic flow from pressure in humans using a nonlinear, three-element model,” Journal of Applied Physiology, vol. 74, no. 5, pp. 2566–2573, 1993.

[24] G. J. Langewouters, K. H. Wesseling, and W. J. A. Goedhard, “The static elastic properties of 45 human thoracic and 20 abdominal aortas in vitro and the parameters of a new model,” Journal of Biomechanics, vol. 17, no. 6, pp. 425–435, 1984.

[25] R. B. P. de Wilde, J. J. Schreuder, P. C. M. van den Berg, and J. R. C. Jansen, “An evaluation of cardiac output by five arterial pulse contour techniques during cardiac surgery,” Anesthesia, vol. 62, no. 8, pp. 760–768, 2007.

[26] M. S. Pitt, P. Marshall, J. P. Diesch, and R. Hainsworth, “Cardiac output by Portapres,” Clinical Science, vol. 106, no. 4, pp. 407–412, 2004.

[27] N. van Dijk, I. G. J. M. de Bruin, J. Gisolf et al., “Hemodynamic effects of leg crossing and skeletal muscle tensing during free standing in patients with vasovagal syncope,” Journal of Applied Physiology, vol. 98, no. 2, pp. 584–590, 2005.

[28] M. P. M. Harms, K. H. Wesseling, F. Pott et al., “Continuous stroke volume monitoring by modelling flow from non-invasive measurement of arterial pressure in humans under orthostatic stress,” Clinical Science, vol. 97, no. 3, pp. 291–301, 1999.

[29] J. J. van Lieshout, K. Toska, E. J. van Lieshout, M. Eriksen, L. Walloe, and K. H. Wesseling, “Beat-to-beat noninvasive stroke volume from arterial pressure and Doppler ultrasound,” European Journal of Applied Physiology, vol. 90, no. 1-2, pp. 131–137, 2003.

[30] W. T. Jellema, K. H. Wesseling, A. B. J. Groeneveld, C. P. Stoutenbeek, L. G. Thijs, and J. J. Van Lieshout, “Continuous
cardiac output in septic shock by simulating a model of the aortic input impedance: a comparison with bolus injection thermodilution,” *Anesthesiology*, vol. 90, no. 5, pp. 1317–1328, 1999.

[31] M. Brignole, P. Alboni, D. Benditt et al., “Guidelines on management (diagnosis and treatment) of syncope,” *European Heart Journal*, vol. 22, no. 15, pp. 1256–1306, 2001.

[32] B. Verheyden, H. Ector, A. E. Aubert, and T. Reybrouck, “Tilt training increases the vasoconstrictor reserve in patients with neurally mediated syncope evoked by head-up tilt testing,” *European Heart Journal*, vol. 29, no. 12, pp. 1523–1530, 2008.

[33] B. Verheyden, J. X. Liu, N. van Dijk et al., “Steep fall in cardiac output is main determinant of hypotension during drug-free and nitroglycerine-induced orthostatic vasovagal syncope,” *Heart Rhythm*, vol. 5, no. 12, pp. 1695–1701, 2008.

[34] A. Kamiya, S. Iwase, H. Kitazawa, and T. Mano, “Muscle sympathetic nerve activity (MSNA) after 120 days of 6 degrees head-down bed rest (HDBR),” *Environmental Medicine*, vol. 43, no. 2, pp. 150–152, 1999.

[35] K. Hirayani, A. Kamiya, S. Iwase et al., “Autonomic cardiovascular changes during and after 14 days of head-down bed rest,” *Autonomic Neuroscience: Basic and Clinical*, vol. 110, no. 2, pp. 121–128, 2004.

[36] G. K. Prisk, H. J. B. Guy, A. R. Elliott, R. A. Deutschman III, and J. B. West, “Pulmonary diffusing-capacity, capillary blood-volume, and cardiac-output during sustained microgravity,” *Journal of Applied Physiology*, vol. 75, no. 1, pp. 15–26, 1993.

[37] A. R. Elliott, G. K. Prisk, H. J. B. Guy, and J. B. West, “Lung volumes during sustained microgravity on spacelab SLS-1,” *Journal of Applied Physiology*, vol. 77, no. 4, pp. 2005–2014, 1994.

[38] A. Pavy-Le Traon, F. Louisy, P. Vasseur-Clausen, A. Gueill, and C. Gharib, “Contributory factor to orthostatic intolerance after simulated weightlessness,” *Clinical Physiology*, vol. 19, no. 5, pp. 360–368, 1999.

[39] V. A. Convertino, D. F. Doerr, and S. L. Stein, “Changes in size and compliance of the calf after 30 days of simulated microgravity,” *Journal of Applied Physiology*, vol. 66, no. 3, pp. 1509–1512, 1989.

[40] G. C. Butler, H. Xing, D. R. Northey, and R. L. Hughson, “Reduced orthostatic tolerance following 4 h head-down tilt,” *European Journal of Applied Physiology and Occupational Physiology*, vol. 62, no. 1, pp. 26–30, 1991.

[41] J. Gisolf, B. E. Westerhof, N. van Dijk, K. H. Wesseling, W. Wieling, and J. M. Karemaker, “Sublingual nitroglycerin used in routine tilt testing provokes a cardiac output-mediated vasovagal response,” *Journal of the American College of Cardiology*, vol. 44, no. 3, pp. 588–593, 2004.

[42] P. Arbeille, P. Kerbeci, D. Greaves, S. Schneider, A. Hargens, and R. Hughson, “Arterial and venous response to Tilt with LBNP test after a 60 day HDT bedrest (WISE study),” *Journal of Gravitational Physiology*, vol. 14, no. 1, pp. 47–48, 2007.

[43] J. M. Fritsch, J. B. Charles, B. S. Bennett, M. M. Jones, and D. L. Eckberg, “Short-duration spaceflight impairs human carotid baroreceptor-cardiac reflex responses,” *Journal of Applied Physiology*, vol. 73, no. 2, pp. 664–671, 1992.

[44] J. M. Fritsch-Yelle, J. B. Charles, M. M. Jones, L. A. Brightol, and D. L. Eckberg, “Spaceflight alters autonomic regulation of arterial pressure in humans,” *Journal of Applied Physiology*, vol. 77, no. 4, pp. 1776–1783, 1994.

[45] W. H. Cooke, J. E. Ames IV, A. A. Crossman et al., “Nine months in space: effects on human autonomic cardiovascular regulation,” *Journal of Applied Physiology*, vol. 89, no. 3, pp. 1039–1045, 2000.

[46] J. M. Fritsch-Yelle, J. B. Charles, M. M. Jones, and M. L. Wood, “Microgravity decreases heart rate and arterial pressure in humans,” *Journal of Applied Physiology*, vol. 80, no. 3, pp. 910–914, 1996.

[47] A. L. Goldberger, M. W. Bungo, R. M. Baevsky et al., “Heart rate dynamics during long-term space flight: report on Mir cosmonauts,” *American Heart Journal*, vol. 128, no. 1, pp. 202–204, 1994.

[48] J. C. Buckley Jr., F. A. Gaffney, L. D. Lane et al., “Central venous pressure in space,” *Journal of Applied Physiology*, vol. 81, no. 1, pp. 19–25, 1996.

[49] N. Foldager, T. A. E. Andersen, F. B. Jessen et al., “Central venous pressure in humans during microgravity,” *Journal of Applied Physiology*, vol. 81, no. 1, pp. 408–412, 1996.

[50] R. Videbaek and P. Norsk, “Atrial distension in humans during microgravity induced by parabolic flights,” *Journal of Applied Physiology*, vol. 83, no. 6, pp. 1862–1866, 1997.