Effect of Ischemic Preconditioning on the Recovery of Cardiac Autonomic Control From Repeated Sprint Exercise

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Repeated sprint exercise (RSE) acutely impairs post-exercise heart rate (HR) recovery (HRR) and time-domain heart rate variability (i.e., RMSSD), likely in part, due to lactic acidosis-induced reduction of cardiac vagal reactivation. In contrast, ischemic preconditioning (IPC) mediates cardiac vagal activation and augments energy metabolism efficiency during prolonged ischemia followed by reperfusion. Therefore, we investigated whether IPC could improve recovery of cardiac autonomic control from RSE partially via improved energy metabolism responses to RSE. Fifteen men team-sport practitioners (mean ± SD: 25 ± 5 years) were randomly exposed to IPC in the legs (3 × 5 min at 220 mmHg) or control (CT; 3 × 5 min at 20 mmHg) 48 h, 24 h, and 35 min before performing 3 sets of 6 shuttle running sprints (15 + 15 m with 180° change of direction and 20 s of active recovery). Sets 1 and 2 were followed by 180 s and set 3 by 360 s of inactive recovery. Short-term HRR was analyzed after all sets via linear regression of HR decay within the first 30 s of recovery (T30) and delta from peak HR to 60 s of recovery (HRR60s). Long-term HRR was analyzed throughout recovery from set 3 via first-order exponential regression of HR decay. Moreover, RMSSD was calculated using 30-s data segments throughout recovery from set 3. Energy metabolism responses were inferred via peak pulmonary oxygen uptake (VO2peak), peak carbon dioxide output (VCO2peak), peak respiratory exchange ratio (RERpeak), first-order exponential regression of VO2 decay within 360 s of recovery and blood lactate concentration ([Lac-]). IPC did not change T30, but increased HRR60s after all sets (condition main effect: P = 0.03; partial eta square (η²p) = 0.27, i.e., large effect size). IPC did not change long-term HRR and RMSSD throughout recovery, nor did IPC change any energy metabolism parameter. In conclusion, IPC accelerated to some extent the short-term recovery, but did not change the long-term recovery of cardiac autonomic control from RSE, and such accelerator effect was not accompanied by any IPC effect on surrogates of energy metabolism responses to RSE.

Keywords: ischemia, supramaximal exercise, parasympathetic, heart beat, metabolism
INTRODUCTION

Training with repeated sprint exercise (RSE) requires less time per session (Stork et al., 2017) and induces similar or even superior feelings of satisfaction (Stork et al., 2017) and aerobic adaptations (Gist et al., 2014) compared to continuous endurance training. Sprint-based training has therefore been considered as a valuable strategy to improve health-related physical fitness of subjects with little time available to engage in regular programs of exercise training (Gist et al., 2014; Stork et al., 2017). However, heart rate (HR) recovery (HRR) is acutely slower and recovery of time domain heart rate variability (HRV) is acutely blunted post-RSE as compared with post-moderate continuous exercise matched to net energy expenditure (Buchheit et al., 2007; Nakamura et al., 2009; Del Rosso et al., 2017). Of note, the acute slowing of HRR after RSE may raise clinical concerns, because slow HRR from maximal exercise, particularly within the first 60 s of recovery (i.e., short-term recovery), is strongly associated with increased risk of cardiac events in subjects with cardiovascular risk factors (Cole et al., 1999).

Post-exercise HRR and HRV are assumed to be mostly determined by interplay between cardiac vagal reactivation and sympathetic withdrawal to the sinus node (Goldberger et al., 2006; Coote, 2010; Peçanha et al., 2014). Thus, methods that improve the cardiac autonomic control could possibly attenuate the acute effect of RSE on post-exercise HRR and HRV. In this context, non-lethal brief cycles of ischemia-reperfusion [i.e., ischemic preconditioning (IPC)] at a site (e.g., limb) induce powerful protection against injury provoked by prolonged ischemia and subsequent reperfusion at a remote site (e.g., heart) (Kharbanda et al., 2002), and the vagal branch of the autonomic nervous system seems to play a pivotal role in such IPC-mediated protection. The reason is that, in rats, vagotomy (Basalay et al., 2012), blockade of muscarinic receptors with atropine (Mastitskaya et al., 2012) or optogenetic silencing of vagal pre-ganglionic neurons (Mastitskaya et al., 2012) nullified the IPC protection against ischemia-reperfusion injury. In addition, IPC not only protects against injury, but may improve some healthy phenotypes (Cocking et al., 2018; Jeffries et al., 2018). For instance, IPC increased resting high-frequency HRV (i.e., a surrogate of cardiac vagal control) in healthy uninjured men (Enko et al., 2011). Therefore, evidence from both ischemia-reperfusion models and healthy resting humans supports that IPC exerts an excitatory effect on the vagal branch of the autonomic nervous system. However, it remains untested whether IPC accelerates post-exercise HRR and augments post-exercise time domain HRV, particularly during the short-term recovery period, in which HRR and time domain HRV are mostly determined by the vagal control of the heart. Testing this issue in healthy humans could then motivate further studies in subjects at risk for cardiovascular events, in case the IPC shows a promising beneficial effect.

If IPC improves post-exercise HRR and time-domain HRV, the IPC effect could be mediated by two non-excluding possibilities. On the one hand, mechanisms that mediate the IPC vagal excitation in models of ischemia-reperfusion injury could play a role (Gourine and Gourine, 2014). These mechanisms include activation of afferent pain fibers at the preconditioned site, as well as release of substances in the circulation from the preconditioned site (Gourine and Gourine, 2014). Thus, one plausible hypothesis is that neural and humoral mechanisms triggered at the preconditioned site could directly activate cardiac vagal neurons leading to a possible beneficial effect of IPC on post-exercise HRR and time domain HRV. On the other hand, IPC could improve post-exercise HRR and time domain HRV via reduction of the exercise-induced energy metabolism distress, which could indirectly increase the cardiac vagal control. Two sets of evidence support such energy metabolism hypothesis. Firstly, manipulation of the aerobic and anaerobic lactic energy contribution to the total energy expenditure of exercise showed that the lower the contribution of the anaerobic lactic metabolism, the faster is the HRR (Buchheit et al., 2007; Nakamura et al., 2009; Del Rosso et al., 2017). The underlying reason for this phenomenon is unknown, but it may involve less metabolites buildup leading to less activation of metabolite-sensitive receptors like muscle metaboreceptors and carotid chemoreceptors (Buchheit et al., 2007). Secondly, IPC augments energy metabolism efficiency in skeletal muscles of pigs exposed to prolonged ischemia (Pang et al., 1995), presumably due to increased efficiency of the mitochondrial electron transport chain (Garlid et al., 2003; Thaveau et al., 2007; Cabrera et al., 2012). Furthermore, some studies have reported IPC to increase peak pulmonary oxygen uptake (VO_{2}p) (de Groot et al., 2010; Cruz et al., 2015) and decrease blood lactate concentration [Lac-] (Bailey et al., 2012) during incremental dynamic exercise in moderately trained subjects, suggesting increased aerobic and decreased anaerobic lactic contribution to exercise energy metabolism. Others have reported IPC not to modify energy metabolism responses to RSE (Patterson et al., 2015; Griffin et al., 2018), but perhaps the IPC dose (1-day exposure) that was effective for incremental dynamic exercise may not be sufficient for RSE. Herein, we chose to test the later hypothesis (i.e., energy metabolism hypothesis) and we employed an IPC dose (3-day exposure) greater than previous studies that investigated the IPC effect on energy metabolism responses to RSE (Patterson et al., 2015; Griffin et al., 2018). Thus, we investigated whether repeated exposure to IPC could improve recovery of cardiac autonomic control from RSE partially via improved energy metabolism responses to RSE.

METHODS

Subjects

Fifteen healthy men participated in the study (mean ± standard deviation: 25 ± 5 years, 81.2 ± 9.7 kg and 179.3 ± 7.4 cm). Subjects were engaged in some type of physical training at least three times a week during the last year and in non-professional team sport competitions (e.g., soccer and basketball). All subjects provided written informed consent before participating in the study. The study conformed to the Declaration of Helsinki and was approved by the Ethics Committee of the Federal University of São Paulo (process number: 192.224).
Experimental Design

The study was single-blinded, cross-over, randomized and controlled. Each subject visited the laboratory on seven occasions (Figure 1). Just one subject was assessed at a time. The first visit was used for familiarization and measurement of the best time in a 30-m sprint, with a change of direction of 180° at the middle of the course (i.e., 15 + 15 m). Subjects had three to six trials, separated by 180 s of inactive recovery, to achieve their best time (BT). Then, the BT served as reference in the RSE task to check an all-out pacing strategy. Exposure to IPC and CT occurred on three occasions, 48 and 24 h before the RSE task, as well as on the day of the RSE task. The last exposure to IPC and CT finished 35 min before the onset of the RSE task. Likewise previous studies (de Groot et al., 2010; Crisafulli et al., 2011; Bailey et al., 2012; Barbosa et al., 2015; Cruz et al., 2015; Del Rosso et al., 2017), subjects were not informed about the study hypothesis in an attempt of blinding, RSE was performed in a sports court, at the same time of the day, with interval between each test of at least 7 and most 14 days. Subjects were instructed to eat a light meal 2 h before RSE, as well as not to train and consume caffeine and alcohol 24 h before RSE.

Ischemic Preconditioning and Control

IPC was performed with subjects seated using customized cuffs which were specifically made to occlude the circulation at the tights (Ferreira et al., 2016). One cuff was used per tight. The cuff had two independent bladders mounted in series. Each bladder was 36 cm long and 17.5 cm wide. Together the bladders covered at least 80% of a thigh’s circumference. An aneroid manometer and an inflation bulb were attached to each bladder. Each cuff had a Velcro strap which, in most cases, surrounded a tight at least two times. In the IPC procedure, cuffs were inflated one at a time to 220 mmHg for 5 min. A total of three inflation/deflation cycles were performed per leg (de Groot et al., 2010). Cuff inflation generally took 15–25 s. Occlusion time started to be counted after the target pressure was achieved. In the CT procedure, cuffs were inflated to 10 mmHg for 5 min and deflated to 0 mmHg for 5 min.

The target IPC inflation pressure of 220 mmHg should be more than enough to cause arterial and venous occlusion in the tights of normotensive subjects using large cuffs as ours. Even so, we used a vascular Doppler (Doppler vascular 610B, MEDMEGA, Brazil) to guarantee the presence of arterial occlusion. The site that yielded the best blood flow signal at the posterior tibial artery was identified at the beginning of each experimental day. The skin was marked at this site. The head of the Doppler transducer was positioned at the marked site at pre-inflation and maintained at this place while a cuff was inflated. The signal usually disappeared when the cuff pressure achieved 140–160 mmHg. Thus, at the target pressure no flow signal was present in any inflation in any subject.

IPC yields two windows of protection against ischemia-reperfusion injury (Hausenloy and Yellon, 2010). The first begins immediately after the IPC exposure and lasts about 2 h (Hausenloy and Yellon, 2010). The second begins approximately 12–24 h after the IPC exposure and can last for 48–72 h (Hausenloy and Yellon, 2010). Of note, repeated exposure to IPC before the second window effect is over has been shown to amplify the IPC effect on the resting vascular function in humans (Loukogeorgakis et al., 2005; Jones et al., 2014). Although an effective dose and timing of IPC administration has not yet been determined for the sake of improvement of exercise-related responses, evidence indicates that the IPC ergogenic effect may last for many hours (Lisbôa et al., 2017). Hence, in the present study, IPC was applied on two consecutive days before, as well as on the day of the RSE task in an attempt to sum early and late effects of IPC (Loukogeorgakis et al., 2005), which could amplify the IPC effect (Jones et al., 2014). However, the use of this design precluded identification of the effective dose of IPC (i.e., the effects from just the acute or repeated exposure could be responsible).

Repeated Sprint Exercise

The warm-up began 10 min after IPC or CT exposure. The warm-up consisted of a standardized and supervised exercise routine that lasted 15 min, including moderate intensity running (5 min), athletic drills (Anfsersen and Skipping), dynamic stretching and four maximal accelerations (15 m) with a change of direction at the end (180°), separated by 1 min of active recovery (walking). Once the warm-up ended, a portable metabolic analyzer (K4b2, Cosmed, Italy) was placed in the subjects, which usually took approximately 10 min.

The RSE task consisted of three sets (i.e., bouts) of six sprints. Each sprint was 30-m long, with a change of direction of 180° at the middle of the course (15 + 15 m). There were 20 s of active recovery between sprints, 180 s of inactive recovery between sets and 360 s of inactive recovery after the last set. During the active recovery, subjects slowed down (10 m), scrolled through a 24-m course during 15–17 s, and then waited for 3–5 s at the start position for the sound signal of the next sprint (Supplementary Video 1). Sound signals were automatically emitted by a photocell system (Test Speed 6.0, CEFISE, Brazil). Pace at the recovery course was verbally informed in order to maintain a correct scroll rhythm. At the end of each set, subjects rapidly slowed down and sat on a chair positioned beside the recovery course (10 m after the finish line).

Subjects were instructed to run as fast as possible during every sprint and were verbally encouraged throughout the test. The researcher that gave verbal encouragement was blinded to the IPC or CT exposure. Subjects had to achieve in the first sprint of the first set at least 95% of their BT obtained in the familiarization visit. Importantly, RSE has been shown to be reproducible and valid for assessing repeated sprint ability in team sports athletes (Rampinini et al., 2007; Impellizzeri et al., 2008). In addition, the protocol with multiple sets of RSE was chosen because it may resemble more accurately what occurs during team sports games (Serpiello et al., 2011).

Measurements

HR was recorded beat by beat (S810i, Polar, Finland) and pulmonary gas exchange breath by breath (K4b2, Cosmed, Italy) throughout the RSE task (Hauswirth et al., 1997; Gamelin et al., 2006; Vanderlei et al., 2008; Weippert et al., 2010). However, due to technical problems we did not record long-term HRR data from one subject and VO2 data from three...
subjects. Before each test, O\textsubscript{2} and CO\textsubscript{2} analyzers were calibrated according to the manufacturer’s specifications using ambient air and gases with known concentration (16% O\textsubscript{2} and 4% CO\textsubscript{2}). The flowmeter was calibrated using a 3-L syringe. An ointment was used in an ear lobe to induce vasodilation at pre-interventions and pre-RSE (Finalgon, Boehringer Mannheim, Germany). Then, a capillary blood sample (25 µL) was collected from the earlobe in a heparinized and calibrated capillary before the exposure to IPC and CT, as well as at 180 s of recovery after each RSE set. Each blood sample was stored in an Eppendorf containing 50 µL of 1% NaF (i.e., anticoagulant) and frozen at −20°C until analysis of blood lactate concentration ([Lac−]).

Time of each sprint was measured with an accuracy of 0.001 s via the photocell system (Test Speed 6.0, CEFISE, Brazil). A photocell was placed 50 cm above the ground. Subjects had to stay 30 cm behind the photocell to avoid a false start at sprint departure.

**Data Analysis**

R-R intervals were extracted from the heart rate monitor and placed in a customized Excel spreadsheet. The difference between consecutive R-R intervals varied from 0 to 20% for 99% of all R-R intervals recorded in the study (29,636 R-R intervals). As we assessed young healthy mean, abnormal data most probably represented measurement artifacts due to bad contact between the thorax strip and the underlying skin, rather than extra-systoles. Abnormal data were objectively identified by an automatic filter that highlighted any R-R interval differing more than 20% from the previous one. This procedure should preserve the physiological variability between successive R-R intervals, while removing artifacts and unlikely extra-systoles (Task Force, 1996). Abnormal data were then deleted and replaced by linear interpolation of adjacent data.

HRR from exercise shows a biphasic pattern consisting on a fast HR decay, which lasts about 60 s (Peçanha et al., 2014), followed by a slow HR decay, which is usually analyzed up to 360 s of recovery (Peçanha et al., 2014). Therefore, HR data recorded during the first 60 s of recovery from sets 1, 2 and 3 were used to calculate the following short-term indexes of the cardiac autonomic control (Buchheit et al., 2007; Nakamura et al., 2009; Peçanha et al., 2014): (1) negative reciprocal of the slope obtained from a linear regression between natural log-transformed HR and time using data from the first 30 s of recovery (T30); (2) absolute difference between 5-s mean HR at the end of a set (HRpeak) and 60 s later (HRR60s). HR data recorded until 360 s of recovery after set 3 were used to calculate a time constant (Tau) of a first-order exponential decay regression. HRR Tau therefore represented a long-term index of the cardiac autonomic control (Buchheit et al., 2007; Nakamura et al., 2009; Peçanha et al., 2014). In addition, RMSSD of 30 s data segments (i.e., RMSSD) provided an index of HRV from the onset to the end of set 3 recovery (Buchheit et al., 2007; Nakamura et al., 2009; Peçanha et al., 2014). T30, HRR60s and RMSSD were calculated in a customized Excel spreadsheet. Tau was calculated in the Origin 6.0 software (Microcal, USA). T30, HRR60s, Tau and RMSSD have shown to be valid indexes of cardiac autonomic control at post-exercise via pharmacological blockade studies (Imai et al., 1994; Goldberger et al., 2006). The reported coefficient of variation for these indexes after high-intensity intermittent exercise is: T30 = 73% (Dupuy et al., 2012), HRR60s = 11% (Bonato et al., 2018), Tau = 14% (Bonato et al., 2018) and RMSSD = 15–28% (Al Haddad et al., 2011). The investigator that analyzed all the data (T.R.L.) was not blinded to the conditions. However, raw R-R
intervals were objectively processed. Then, data were used for calculations using fixed mathematical parameters. Therefore, no step in the analysis process of R-R intervals was vulnerable to subjective data handling, and the same applies to the breath data analysis described next.

Breathing data were filtered to exclude aberrant breaths (two standard deviations from the mean of a 30-breath window) (Poole and Jones, 2012). Valid breath by breath values were linearly interpolated to get one value per second (Origin 6.0, Microcal, USA). Then, 5-s means were calculated. Peak oxygen uptake (VO2peak) and carbon dioxide output (VCO2peak) were taken as: (1) the highest 5-s mean of the last sprint of each set, and (2) the mean of the three highest 5-s values of each set. The two analyses provided similar results' interpretation, and so only the results from the former were presented. Peak respiratory exchange ratio (RERpeak) was calculated dividing ˙VCO2 peak by VO2peak. Kinetics of long-term VO2 recovery was represented by the Tau of a first-order exponential decay regression using VO2 data from the end of set 3 to the end of the subsequent 360-s recovery period (Rossiter et al., 2002). VO2 recovery kinetics was measured because of its association with phosphocreatine recovery kinetics (Rossiter et al., 2002), which, in turn, is largely dependent on the oxidative metabolism (Piiper and Spiller, 1970). Accumulation of blood [Lac-] (Δ[Lac-]) was quantified via deltas of two consecutive measurements (i.e., set 1 minus baseline; set 2 minus set 1; and set 3 minus set 2). At last, the following parameters were obtained to assess RSE performance: BT, total time (TT) and percent sprint performance decrement (%DC). The %DC was determined as follows: (100*(TT/ BT*6)) - 100 (Fitzsimons et al., 1993). The reported coefficient of variation for the BT, TT and %DC is 1.3, 0.8, and 30.2%, respectively (Impellizzeri et al., 2008).

Statistical Analysis
Sample size was calculated taking into account a two-way repeated measures ANOVA with two interventions (IPC and CT) and three repeated measures (sets 1, 2, and 3). The main endpoint was the HRR60s, given that this is valid (Kannankeril et al., 2004), reproducible (Al Haddad et al., 2011; Dupuy et al., 2012; Bonato et al., 2018) and widely used in clinical and sports settings to assess the post-exercise cardiac autonomic control (Buchheit, 2014; Peçanha et al., 2014). High-intensity interval training protocols provoked significant HRR60s increase (P < 0.05) at d effect size of 0.75 (Lamberts et al., 2009) and 0.87 (Villelabeitia-Jaureguizar et al., 2017). Both effects corresponded to an absolute increase of 6 bpm. We reasoned the IPC effect on HRR60s could be approximately half of such effects (d~0.40; absolute delta ~ 3 bpm). Next, the estimated d effect size had to be converted to a partial eta square (ηp²) effect size to input an estimated effect in a repeated measures ANOVA. This resulted in a ηp² of 0.04. Correlation among repeated measures was at 0.85 and nonsphericity correction at 1.0. Using these parameters, 14 subjects would be necessary to find a P-value lower than 0.05, with 0.80 of power (G*Power 3.1, Dusseldorf University, Germany).

Data distribution was verified by the Shapiro-Wilk’s test. RMSSD did not present normal distribution, and so, was transformed to natural logarithm for inferential analyses. Paired Student’s t-test was used to analyze HRR Tau, baseline [Lac-] and VO2 Tau. Two-way repeated measures ANOVA (factors: condition and set) was used to analyze HRpeak, short-term HRR, VO2peak, VCO2peak, RERpeak, [Lac-], Δ[Lac-], and RSE performance. Two-way repeated measures ANOVA (factors: condition and time) was used to analyze 5-s mean HR and RMSSD along 360 s after set 3. Three-way repeated measures ANOVA (factors: condition, set and time) was used to analyze 5-s mean HR and HRR60s throughout 60-s recovery periods after all sets. The Greenhouse-Geisser’s correction was used to adjust ANOVA results, whenever sphericity was violated in the Mauchly’s test. The LSD post hoc was used when significant F values were found. Effect sizes for Student’s t-test and ANOVA results were calculated as Cohen’s d and ηp², respectively. The following thresholds were used for d and ηp² interpretation (Cohen, 1988): d, trivial > 0.00; small > 0.20; medium > 0.50; and large > 0.8/ηp², trivial > 0.00; small > 0.01; medium > 0.06; large > 0.14. Results are presented as mean ± standard error of mean (SEM). Statistical significance was set at P < 0.05. Statistical analyses were performed in the software Statistica 12 (Statsoft, EUA).

RESULTS
HR from peak to 25 s of recovery was similar between IPC and CT in all sets (Table 1 and Figure 2), leading to similar T30 (Table 1). On the other hand, HR from 30 to 60 s of recovery was lower (medium ηp²) in the IPC than CT in all sets (Figure 2), and, consequently, IPC increased HRR60s (Table 1; large ηp²; change = 12.8%, 95% CI = 5.8–19.7%). HR values were similar between conditions throughout 360 s of recovery from set 3 (Figure 3), resulting in similar HRR Tau (Table 1). RMSSD was also similar between IPC and CT throughout the entire recovery from set 3 (Figure 4). No difference between IPC and CT was observed for baseline [Lac-] (IPC: 1.30 ± 0.16 mmol.L⁻¹ and CT: 1.24 ± 0.15 mmol.L⁻¹; P = 0.49; d = 0.20), as well as for VO2peak, VCO2peak, RERpeak, [Lac-] and Δ[Lac-] and VO2 Tau (Table 2). Additionally, RSE performance was similar between conditions (Table 3).

DISCUSSION
Our main finding was that IPC increased HRR60s which, in addition to being a valid (Kannankeril et al., 2004) and reproducible parameter (Al Haddad et al., 2011; Dupuy et al., 2012; Bonato et al., 2018), is the most used method to assess the post-exercise cardiac autonomic control in clinical and sports settings (Buchheit, 2014; Peçanha et al., 2014). This result is novel and may therefore have practical implications. However, contrary to our hypothesis, the IPC-mediated cardiac autonomic control improvement was not accompanied by changes in VO2, VCO2, RER, and blood [Lac-]. Thus, collectively, the results indicate that IPC improved an important index of the short-term recovery of cardiac autonomic control from RSE, regardless of change in surrogates of energy metabolism responses to RSE.
TABLE 1 | Peak heart rate (HRpeak), short-term and long-term heart rate recovery (HRR) after each set of repeated sprint.

| SET 1 | SET 2 | SET 3 | ANOVA P-value ($\eta^2_p$) | Student’s t-test P-value (d) |
|-------|-------|-------|---------------------------|----------------------------|
|       |       |       | Condition | Set | Interaction |       |       |
| HRpeak (bpm) |       |       |            |     |             |       |       |
| CT    | 181 ± 2 | 183 ± 2 | 185 ± 2 | 0.76 (0.01) | 0.01 (0.33) | 0.14 (0.14) | NA |
| IPC   | 182 ± 2 | 183 ± 2 | 185 ± 2 |             |             |             |         |
| T30 (s) |       |       |            |     |             |       |       |
| CT    | 435 ± 81 | 434 ± 55 | 407 ± 48 | 0.15 (0.16) | 0.42 (0.07) | 0.48 (0.04) | NA |
| IPC   | 365 ± 56 | 427 ± 65 | 374 ± 47 |             |             |             |         |
| HRR60s (bpm) |       |       |            |     |             |       |       |
| CT    | 34 ± 3  | 33 ± 2  | 34 ± 3   | 0.03 (0.27) | 0.24 (0.09) | 0.69 (0.03) | NA |
| IPC   | 39 ± 3  | 36 ± 3  | 38 ± 3   |             |             |             |         |
| HRR TAU (s) |       |       |            |     |             |       |       |
| CT    | NA     | NA     | 78 ± 4   | NA     | NA         | NA     | 0.64 (--0.14) |
| IPC   | 78 ± 6 |       |           |         | NA         | NA     |         |

Data are mean ± SEM. T30, negative reciprocal of the slope obtained from a linear regression between natural log-transformed heart rate (HR) and time using data from the first 30 s of recovery; HRR60s, absolute difference between 5-s mean HR at the end of a set and 60 s later; Tau, time constant of a first-order exponential decay regression after set 3; CT, control; IPC, ischemic preconditioning; $\eta^2_p$, partial eta square; NA, not applicable; HRpeak, T30 and HRR60s n = 15; HRR Tau n = 14.

Effect of IPC on Post-exercise Cardiac Autonomic Control

In our study IPC did not change HRpeak. This finding is similar to those reported by studies that investigated the IPC effect on HRpeak during high-intensity intermittent exercise (Marocolo et al., 2017; Zinner et al., 2017) or HRpeak during ramp incremental exercise (de Groot et al., 2010; Crisafulli et al., 2011; Sabino-Carvalho et al., 2017). As far as we know, only two studies
have reported the IPC effect on post-exercise cardiovascular parameters. Both studies used handgrip exercise and employed circulatory occlusion during recovery from exercise to isolate the activation of the muscle metaboreflex. Incognito et al. (2017) reported IPC did not change arterial pressure, HR and muscle sympathetic nerve activity during exercise and post-exercise circulatory occlusion. Mulliri et al. (2016) reported IPC did not change central and peripheral hemodynamic parameters. Both studies used handgrip exercise and employed circulatory occlusion during recovery from exercise to isolate the activation of the muscle metaboreflex. Incognito et al. (2017) reported IPC did not change arterial pressure, HR and muscle sympathetic nerve activity during exercise and post-exercise circulatory occlusion. Mulliri et al. (2016) reported IPC did not change arterial pressure, HR and muscle sympathetic nerve activity during exercise and post-exercise circulatory occlusion. Of note, however, Incognito et al. (2017) and Mulliri et al. (2016) did not provide enough data to interpret the IPC effect under normal free flow recovery from exercise, like we did in the present study. In addition, cardiovascular responses to handgrip exercise are very different from those provoked by dynamic exercise involving large muscle mass (Lewis et al., 1985). For example, Incognito et al. (2017) and Mulliri et al. (2016) reported mean HR to achieve 102 and 72 bpm, respectively. In contrast, in our study HR surpassed 180 bpm. Therefore, methodological dissimilarities preclude comparison of the IPC effect on post-exercise cardiovascular parameters between former studies (Mulliri et al., 2016; Incognito et al., 2017) and the present one.

We found that IPC did not change HRR up to 25 s, T30, HRR Tau and RMSSD. Conversely, IPC consistently lowered HR from 30 to 60 s, leading to increased HRR60s after all sets. Thus, our results indicate that IPC only had an effect on the second half of the short-term HRR. A possible explanation for the divergent IPC effect on short-term HRR indexes is that the RSE deleterious effect on HRR was so powerful that HR did not decay within approximately the first 10 s of recovery (i.e., onset HRR). As a result, the T30 index which relies on onset HRR data may have not been sensitive to assess the short-term component of post-RSE HRR. This phenomenon may depend on the exercise intensity, given that it has also been reported by other studies that assessed post-RSE HRR (Buchheit et al., 2007; Nakamura et al., 2009; Del Rosso et al., 2017), but not by studies that assessed HRR after submaximal or maximal incremental exercise in healthy subjects (Imai et al., 1994; Kannankeril et al., 2004). Another point is that the IPC effect in the present study

### TABLE 2 | Energy metabolism responses to repeated sprint exercise.

|                     | SET 1                  | SET 2                  | SET 3                  | ANOVA P-value (\(\eta^2_P\))     |
|---------------------|------------------------|------------------------|------------------------|----------------------------------|
| \(\dot{V}O_2\)peak (\(\text{mL.kg}^{-1}.\text{min}^{-1}\)) | CT                     | 38.45 ± 1.84           | 37.68 ± 1.64           | 36.93 ± 1.93                     | Condition: 0.95 (0.00) Set: 0.14 (0.17) Interaction: 0.98 (0.00) |
|                     | IPC                    | 38.25 ± 1.74           | 37.58 ± 1.51           | 37.02 ± 1.86                     |                                        |
| \(\dot{V}CO_2\)peak (\(\text{mL.kg}^{-1}.\text{min}^{-1}\)) | CT                     | 49.08 ± 1.71           | 44.32 ± 0.88           | 42.50 ± 1.42                     | Condition: 0.80 (0.01) Set: <0.01 (0.63) Interaction: 0.97 (0.00) |
|                     | IPC                    | 49.01 ± 1.28           | 43.96 ± 1.16           | 42.00 ± 1.66                     |                                        |
| RER                 | CT                     | 1.30 ± 0.05            | 1.20 ± 0.05            | 1.18 ± 0.07                      | Condition: 0.78 (0.01) Set: <0.01 (0.63) Interaction: 0.73 (0.03) |
|                     | IPC                    | 1.30 ± 0.05            | 1.19 ± 0.05            | 1.15 ± 0.05                      |                                        |
| [Lac-] (mmol.L\(^{-1}\)) | CT                     | 11.05 ± 0.61           | 14.50 ± 0.96           | 14.54 ± 1.09                     | Condition: 0.81 (0.00) Set: <0.01 (0.70) Interaction: 0.84 (0.01) |
|                     | IPC                    | 11.06 ± 0.82           | 14.12 ± 1.11           | 14.30 ± 1.06                     |                                        |
| \(\Delta\) [Lac-] (mmol.L\(^{-1}\)) | CT                     | 9.82 ± 0.67            | 3.44 ± 0.62            | 0.04 ± 0.41                      | Condition: 0.73 (0.01) Set: <0.01 (0.89) Interaction: 0.89 (0.01) |
|                     | IPC                    | 9.76 ± 0.80            | 3.06 ± 0.52            | 0.18 ± 0.61                      |                                        |

Data are mean ± SEM. \(\dot{V}O_2\)peak, peak oxygen uptake; \(\dot{V}CO_2\)peak, peak carbon dioxide output; \(\dot{R}ER\)peak, peak respiratory exchange ratio; [Lac-], blood lactate concentration; \(\Delta\) [Lac-], difference between consecutive blood lactate measures; CT, control; IPC, ischemic preconditioning; \(\eta^2_P\), partial eta square. \(\dot{V}O_2\)peak, \(\dot{V}CO_2\)peak and \(\dot{R}ER\)peak \(n = 12\). [Lac-] \(\eta^2\) and \(\Delta\) [Lac-] \(n = 15\).
may have not been large enough to overcome the variability of parameters with low-to-moderate reproducibility, such as T30 and RMSSD. On the other hand, the absence of IPC effect on the HRR Tau was unequivocal, due to equal mean values between IPC and CT, high Student’s t-test P-value and reasonable reproducibility of this parameter (Bonato et al., 2018). These facts therefore clearly support that IPC did not change long-term post-RSE HRR.

Previous studies have used systemic pharmacological blockade of vagal (i.e., muscarinic) and sympathetic (i.e., beta) receptors aiming to dissect the contribution of each branch of the autonomic nervous system to HRR (Imai et al., 1994; Kannankeril et al., 2004; Goldberger et al., 2006). These studies showed both short- and long-term HRR are largely determined by cardiac vagal reactivation post-submaximal exercise, with a negligible influence of the sympathetic branch. However, no study has investigated the autonomic contribution to HRR after supramaximal exercise (i.e., exercise performed at velocity or workload higher than peak velocity or workload of an incremental exercise test), such as RSE, which may not be the same as post-maximal exercise. Firstly, because our study and others showed RMSSD almost did not recover post-RSE (Buchheit et al., 2007; Nakamura et al., 2009; Del Rosso et al., 2017), which is not the case post-maximal exercise (Goldberger et al., 2006). Secondly, because the level of circulating catecholamines follows exercise-induced lactic acidosis (Mazzo and Marshall, 1989) and RSE usually leads to greater lactic acidosis than maximal exercise (Buchheit et al., 2007; Sabino-Carvalho et al., 2017). Thirdly, because intense muscle metaboreflex activation during recovery from exercise under circulatory occlusion increases cardiac sympathoexcitation and offsets the influence of cardiac vagal activation on HR (Fisher et al., 2010). In sum, although cardiac vagal reactivation possibly plays a crucial role for short-term post-RSE HRR, sympathoexcitation is greater during RSE than maximal exercise. Consequently, cardiac sympathetic activity perhaps restrains to some extent short-term post-RSE HRR, and cardiac sympathetic withdrawal may importantly contribute to long-term post-RSE HRR. Thus, in our study, IPC-induced acceleration of HRR60s was possibly mediated by greater cardiac vagal reactivation, but lower cardiac sympathetic restraint cannot be disregarded. In contrast, as IPC did not change HRR after 60 s of recovery and RMSSD along 360 s of recovery, cardiac vagal reactivation and, particularly, cardiac sympathetic withdrawal likely did not change during the long-term component of cardiac autonomic control recovery.

### Effect of IPC on Energy Metabolism Responses

IPC increased peak pulmonary oxygen uptake (VO2) in a sample mostly composed by men (de Groot et al., 2010; Cruz et al., 2015) and decreased blood lactate concentration [Lac-] in men (Bailey et al., 2012) during incremental dynamic exercise. In contrast, Patterson et al. (2015) showed no effect of IPC on VO2, VCO2, and blood [Lac-] during twelve 6-s cycling sprints in men. Gibson et al. (2015) reported IPC to reduce blood [Lac-] in women, but not men, post five 6-s cycling sprints. More recently, Griffin et al. (2018) did not find an effect of IPC on blood [Lac-] during three sets of six shuttle run sprints in men. The reason for the dissimilar IPC effect on surrogates of energy metabolism during incremental dynamic exercise vs. RSE is still unclear. One possibility could be that the IPC dose has been insufficient for RSE. Thus, herein we employed a repeated IPC protocol. Nevertheless, we also found that IPC changed none of the assessed surrogates of energy metabolism. This result consequently suggests that the IPC dose may not be an issue. Possible modulators of the IPC effect, such as gender (Gibson et al., 2015), physical fitness (Sabino-Carvalho et al., 2017), and time between IPC application and exercise assessments (Lisbôa et al., 2017) should then be taken into consideration by next studies. Still of note, our study and others (de Groot et al., 2010; Crisafulli et al., 2011; Bailey et al., 2012; Cruz et al., 2015; Gibson et al., 2015; Patterson et al., 2015; Griffin et al., 2018) have measured VO2 and VCO2 via analysis of breathing air and [Lac-] via analysis of capillary blood, but these methods only provide indirect information with regards to muscle aerobic and anaerobic responses. Thus, other methods should be employed in the future to confirm the IPC effect on energy metabolism responses to RSE.

As IPC did not change energy metabolism surrogates during a RSE task, the acceleration of HRR60s was possibly mediated by other factors than energy metabolism responses to RSE. In this sense, IPC has been linked with release of humoral factors by preconditioned tissues (e.g., adenosine, bradykinin, and

### Table 3 | Repeated sprint exercise performance.

| Condition | Set 1 Mean ± SD | Set 2 Mean ± SD | Set 3 Mean ± SD | ANOVA P-value (η²p) |
|-----------|----------------|----------------|----------------|---------------------|
| BT (s)    |                |                |                |                     |
| CT        | 5.9 ± 0.1      | 6.0 ± 0.1      | 6.2 ± 0.1      | 0.23 (0.10)         |
| IPC       | 5.8 ± 0.1      | 6.0 ± 0.2      | 6.1 ± 0.1      | <0.01 (0.55)        |
| TT (s)    |                |                |                |                     |
| CT        | 37.2 ± 0.4     | 38.6 ± 0.4     | 39.4 ± 0.6     | 0.09 (0.19)         |
| IPC       | 36.5 ± 0.3     | 37.9 ± 0.4     | 38.6 ± 0.5     | <0.01 (0.70)        |
| %DC       |                |                |                |                     |
| CT        | 4.4 ± 0.4      | 6.7 ± 0.6      | 6.7 ± 0.8      | 0.07 (0.21)         |
| IPC       | 4.3 ± 0.4      | 5.3 ± 0.5      | 5.8 ± 0.6      | <0.01 (0.40)        |

Data are mean ± SEM. BT, best time; TT, total time; %DC, percent sprint performance decrement; CT, control; IPC, ischemic preconditioning; η²p, partial eta square; n = 15 for all variables.
calcitonin), as well as by activation of afferent neural pathways in preconditioned tissues (e.g., C- and Aδ-fibers) (Gourine and Gourine, 2014). Humoral and neural mechanisms have thus been considered triggers of IPC-induced vagal activation during ischemia-reperfusion injury protocols (Gourine and Gourine, 2014). Therefore, direct vagal activation via neural and humoral mechanisms likely underlies the IPC effect on the HRR60s, rather than an indirect IPC effect on energy metabolism responses to exercise.

Some studies have shown that IPC can enhance exercise performance due to a placebo effect rather than a specific IPC effect (Marocolo et al., 2015, 2016; Sabino-Carvalho et al., 2017). Noteworthy, the IPC placebo effect on exercise performance was not accompanied by change in energy metabolism and HR responses to exercise (Marocolo et al., 2015, 2016; Sabino-Carvalho et al., 2017). Our experimental design did not allow dissecting specific IPC effects from placebo effects. However, based on the aforementioned studies (Clark et al., 2000; Foad et al., 2008; Marocolo et al., 2015, 2016; Sabino-Carvalho et al., 2017), it is possible that sprints time were more prone to placebo and nocebo effects than physiological measurements.

Implications
HRR60s percent change (12.8% for IPC main effect) surpassed the smallest worthwhile change (6%, calculated as 0.2 × between-subjects standard deviation for all sets in the CT condition) and the coefficient of variation elsewhere reported (i.e., 11%) (Bonato et al., 2018). In addition, the HRR60s absolute change in the present study (i.e., 4 bpm) was somewhat comparable to the absolute change provoked by 8 weeks of high-intensity interval training in patients with coronary disease (i.e., 6 bpm) (Villelabeitia-Jaureguizar et al., 2017) and by 3 weeks of high-intensity interval training in well-trained cyclists (i.e., 5 bpm) (Lamberts et al., 2009). The IPC effect herein observed therefore achieved a magnitude that could carry practical implications for clinical populations and athletes which deserves investigation by next studies. With regard to clinical populations, studies in dogs strongly support that the higher the HRR and the cardiac vagal outflow to the heart, the lower is the chance of developing ventricular fibrillation and dyeing after induction of acute myocardial ischemia during exercise (Vanoli et al., 1991; Smith et al., 2005). Although we assessed healthy young men, our results suggest IPC could carry cardioprotective benefits for subjects with cardiovascular risk factors or stablished cardiovascular diseases that engage in RSE training or practice of sports that may involve RSE, such as soccer, basketball, tennis, etc. With regard to athletes, a better post-exercise cardiac autonomic control may indicate greater readiness to train at high-intensity accumulation and running performance. Med. Sci. Sports Exerc. 44, 2084–2089. doi: 10.1249/MSS.0b013e318262cb17

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