MS-proteomics provides insight into the host responses towards alginate microspheres

Abba E. Corona, Davi M. Fonseca, Animesh Sharma, Geir Slupphaug, Berit L. Strand, Anne Mari A. Rokstad

**A R T I C L E   I N F O**

**Keywords:**
- Alginate hydrogel microspheres
- Proteomics
- Protein adsorption
- Complement
- Coagulation
- Immune profiling

**A B S T R A C T**

Protein adsorption to biomaterial surfaces is considered a determining factor for the host response. Here we detail the protein adsorption profiles of alginate hydrogel microspheres relevant for cell therapy using mass spectrometry (MS)-based proteomics. The investigated microspheres include sulfated alginate (SA), high G alginate (HiG), and poly-
lysine coated alginate (AP), which previously have been shown to exhibit different inflammatory and fibrotic responses. The biological significance was assessed in lepirudin-anticoagulated human whole blood (hWB) by functional analysis of the acute-phase responses (complement and coagulation). Proteomic profiling revealed distinct signatures for the microspheres, wherein Ingenuity Pathway Analysis identified complement and coagulation as the top enriched canonical pathways. The levels of complement and coagulation activators and inhibitors were distinctly different, which was reflected in the functional hWB analyses: SA was highly enriched with inhibitory factors of complement and coagulation (e.g. C1 inhibitor, factor H, antithrombin-III, heparin cofactor 2), other heparin-binding proteins and factors promoting fibrinolysis (factor XII, plasma kallikrein), conforming to an anti-inflammatory and anti-fibrotic profile. HiG enriched moderate levels of complement inhibitors, conforming to a low-inflammatory and pro-fibrotic profile. AP showed the most prominent enrichment of complement activators (e.g. C3, properdin, C-reactive protein) and low levels of inhibitors, conforming to a pro-inflammatory and highly pro-fibrotic profile. In conclusion, the extensive enrichment of inhibitory acute-phase proteins on SA could be a determining factor for its reduced host response. The interactions between the plasma proteins and hydrogel surfaces shown herein point to proteomics as an important supplement to existing in vitro and in vivo methods for designing biocompatible alginate-based hydrogels.

**1. Introduction**

The use of alginate hydrogel microspheres for immunosolation in cell therapy holds great promise for treating various medical conditions, e.g. type 1 diabetes or acute liver failure, mitigating the need for systemic immunosuppressive treatment after graft transplantation [1–3]. However, implantation of biomaterials may result in acute and chronic inflammatory responses that lead to fibrotic tissue development, as part of the foreign body response [4]. For microspheres used in cell therapy, pericapsular fibrotic overgrowth (PFO) constitutes a major challenge, in which immune cells (neutrophils, macrophages) and fibroblasts hinder the diffusion of nutrients and oxygen, thus compromising the viability and function of the encapsulated cells [5,6]. Insight into the mechanistic cues associated with PFO will advance the development of high-performance, biocompatible materials for cell and tissue transplantation, with further impact on diagnostic sensors and implants. The initial protein adsorption to implanted biomaterials is considered a determining factor for the subsequent host responses [4,7,8]. Here, we investigate the protein adsorption profiles of three types of alginate microspheres that have previously been used or are promising candidates...
for clinical transplantation [1,9,10], which we recently assessed in terms of inflammatory and fibrotic potentials using in vitro and in vivo models [10]. Proteomics could serve as a complementary method to understand the initial protein adsorption important for the design and selection of alginate microspheres with reduced host responses.

Alginate hydrogels are ionically crosslinked networks (e.g. with Ca\(^{2+}\), Sr\(^{2+}\), Ba\(^{2+}\)) of linear, anionic polysaccharides that consist of (1,4)-linked \(\alpha-L\)-mannuronic (M) and \(\beta-D\)-guluronic (G) residues. The hydrogel is formed under physiological conditions, and the high water content (98–99%) allows for rapid diffusion of nutrients and oxygen to encapsulated cells, ensuring cell viability and function. Although generally regarded as biocompatible, the detailed design of alginate-based microspheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3]. Microspheres that are prone to PFO include the widely studied high G alginate microbeads [1,2,10,11], where the PFO response is exacerbated by coating with polyamines (e.g. that have addressed the adsorption of plasma or serum proteins to spheres ultimately determines the onset of PFO and the long-term function of encapsulated cells in vivo [2,3].

Mass spectrometry (MS)-based proteomic analysis represents an efficient and highly sensitive approach to identify protein adsorption profiles on biomaterial surfaces [7], and thus provides an additional means to predict biological performance and potentially reduce in vivo experimentation. To date, there is a limited number of proteomic studies that have addressed the adsorption of plasma or serum proteins to hydrogels [20,27,28], and neither of these encompassed alginate-based hydrogels or microspheres. Previous studies using MS-based proteomics have linked protein adsorption to the immune reactivity [20] or fibrotic tissue development [27] of poly(ethylene glycol) (PEG) hydrogels. The latter revealed an initial adsorption of acute-phase proteins for highly fibrotic PEG hydrogels explanted from mice [27]. More generally, the high fibrotic potential of PFO (pro-inflammatory and highly fibrotic) and displayed marked C3 deposition in vivo. Here, we present the first study on LC-MS/MS-based quantitative profiling of plasma proteins adsorbed to alginate hydrogels using a physiologically relevant human plasma model. Three types of microspheres were selected based on their different PFO responses and inflammatory potentials known from previous work [10]: HiG (low-inflammatory and fibrotic), SA (low-inflammatory and anti-fibrotic) and AP (pro-inflammatory and highly fibrotic). Unique protein signatures were identified for the different alginate microspheres. Immune profiles of the microspheres were detailed by combining proteomics and functional studies on initial inflammatory responses, with a particular focus on the acute-phase proteins of the complement and coagulation systems.

Materials and methods

2.1. Materials

Ultra-pure (UP) sodium alginites (endotoxin \(\leq 43\) EU/g) were from Novamatrix (Sandvika, Norway). UP-low-viscosity high G (LVG) alginate (68% gulurionate [G], duplet fraction \(F_{DG} = 0.57\), triplet fraction \(F_{DGG} = 0.53\), average G-block length \(N_G > 1\) = 16, weight average molecular weight \(M_w = 237\) kDa) was used as gelling alginate. UP-medium-viscosity high G (MVG) alginate (66% G, \(F_{DG} = 0.55\), \(F_{DG} = 0.50\), \(N_G > 1\) = 13, weight average \(M_w = 235\) kDa) was used to produce sulfated alginate. Determination of the alginate chemical composition by H\(^1\)-NMR [49,50] and molecular weight by SEC-MALLS [51] has previously been described. Preparation of alginites and alginate microspheres included analytical grade CaCl\(_2\), BaCl\(_2\), NaCl, and formamide from Merck (Darmstadt, Germany). Poly-\(L\)-lysine (PLL) hydrochloride \((M_w = 15–50\) kDa) and chitosan (99%) were from Sigma-Aldrich (St. Louis, MO, USA). D(-)-Mannitol was from VWR International BVBA (Leuven,
2.3. Preparation of alginate microspheres

Three different microspheres were prepared using the same alginate formulations as in our recent study on PFO [10], comprising unmodified alginate (HIG), a mixture of 20% sulfated alginate and 80% unmodified alginate (SA), and unmodified alginate with PLL-coating (AP). Alginate solutions (5 mL) of 1.8% (w/v) were dripped into a gelling bath containing 10% (v/v) of 1.8% (w/v) were dripped into a gelling bath containing a gelling solution of 1.8% (w/v) were dripped into a gelling bath containing alginate (SA), and unmodi

2.4. Proteomic sample preparation

2.4.1. Incubation of microspheres in human lepirudin-plasma

Alginate microspheres (50 μL) were incubated in pooled (N = 7) lepirudin-plasma (300 μL) for 2 h at 37 °C under rotation, with five replicates for each type of microsphere. Human blood was anticoagulated by adding lepirudin (50 μg/mL), centrifuged (1800 × g, 15 min), and harvested plasma stored at -80 °C. Control samples comprised microspheres (50 μL) incubated in 300 μL 0.9% NaCl (saline control) and a pooled plasma control sample (10 μL). Low-activating polypropylene vials were used for all samples. Microspheres were in 0.9% NaCl (2 × 500 μL) to remove non-adсорbing proteins. Samples were stored in 0.9% NaCl (100 μL) at 4 °C. The storage solution was removed before analysis.

2.4.2. Primary elution of adsorbed plasma proteins (E-fraction)

Microspheres and control samples were incubated in 2D-PAGE buffer (100 μL, 7.0 M Urea, 2.0 M thiourea, 2.5% CHAPS, 25 mM DTT) for 2 h on a rotary shaker (37 °C, 400 rpm), and eluates were transferred to new tubes. 2D-buffer incubation was repeated (5 min), and the respective eluates were pooled. Eluates were stepwise added methanol (800 μL), chloroform (200 μL) and water (600 μL) with intermittent vortexing, and then centrifuged (16 000 × g, 15 min). The top aqueous layer was removed, and methanol (800 μL) was added, followed by vortexing and centrifugation (16 000 × g, 60 min). The supernatant was removed, and the pellet with remaining solution was evaporated to dryness. 50 mM ammonium bicarbonate (Ambic; 100 μL) was added to the pellet, and samples were vortexed. Supernatants were stepwise added 0.5 M DTT (4 μL, 3 min), 0.2 M iodoacetamide (30 μL, 30 min in the dark), 0.5 M DTT (8 μL, 20 min), incubated overnight on a rotary shaker (37 °C, 400 rpm) in 12.5 ng/μL trypsin in 44 mM Ambic (100 μL), and evaporated to dryness.

2.4.3. On-microsphere trypsination of residual plasma proteins (T-fraction)

Following the primary elution, microspheres were washed in 50 mM Ambic (200 μL) for 1 h on a rotary shaker (24 °C, 400 rpm) and further washed in 50 mM Ambic (2 × 200 μL). Microspheres were added 50 mM Ambic (100 μL) and stepwise treated with DTT/iodoacetamide/DTT as described above. Samples were washed in 50 mM Ambic (200 and 100 μL, respectively), resuspended in 50 mM Ambic (100 μL), and incubated overnight on a rotary shaker (37 °C, 400 rpm) in 12.5 ng/μL trypsin in 44 mM Ambic (100 μL). Released tryptic peptides were transferred to new tubes. Microspheres were washed in 50 mM Ambic (50 μL), and residual released peptides were pooled with respective samples. Tryptic eluates were evaporated to dryness.

2.4.4. Preparation of peptides in E- and T-fractions

Dried peptides were reconstituted in 0.1% formic acid in water (60 μL). Stage tip columns consisting of three C-18 filters were prewashed with methanol (3 × 50 μL), centrifuged (1500 × g, 3 min) for each wash, equilibrated with 0.1% formic acid in water (3 × 100 μL), and centrifuged (1500 × g, 2 min) for each equilibration step. Peptide samples were centrifuged (16 000 × g, 25 min), supernatants loaded onto separate stage tip columns and centrifuged (1500 × g, 4 min). Flow-through solutions were reloaded to stage tip columns and centrifuged (1500 × g, 3 min). Stage tip columns were washed with 0.1% formic acid (2 × 60 μL), centrifuged (1500 × g, 3 min) for each wash, and the column was then discarded. Peptides were eluted from the stage tip column using 0.1% formic acid in 70% acetonitrile (2 × 40 μL), centrifuged (1500 × g, 1 min) for each elution, and evaporated to dryness. Dried peptides were reconstituted in 0.1% formic acid in water (60 μL), vortexed, and agitated for 1–3 h (4 °C, 900 rpm). Samples were centrifuged (16 000 × g, 15 min), and supernatants (30 μL) were transferred to MS-vials for LC-MS/MS analysis.
2.5. Liquid chromatography-tandem mass spectrometry (LC-MS/MS)

LC-MS/MS was performed on an EASY-nLC 1000 UPLC system (Thermo Scientific) interfaced with an Orbitrap Elite mass spectrometer (Thermo Scientific) via a Nanospray Flex ion source (Thermo Scientific). Peptides were injected onto an Acclaim PepMap100C18 trap column (75 μm i.d., 2 cm long, 3 μm, 100 Å, Thermo Scientific) and further separated on an Acclaim PepMap100C18 analytical column (75 μm i.d., 50 cm long, 2 μm, 100 Å, Thermo Scientific) using a 120-min multi-step gradient (3 min 2%-6% B, 92 min 6%-30% B, 5 min 30%-40% B, 5 min 40%-100% B and 15 min at 100% B; where B is 0.1% formic acid in acetonitrile and A is 0.1% formic acid in water) at 250 nL/min. Peptides were analysed in positive ion mode under data-dependent acquisition using the following parameters: Electrospray voltage 2.5 kV, CID fragmentation with normalised collision energy 35 and 10 ms activation time. Each MS scan (400–1600 m/z, 1 m/z isolation width, profile) was acquired at a resolution of 120 000 FWHM in the Orbitrap analyser, followed by rapid MS/MS scans (2 m/z isolation width, centroid) triggered for the 15 most intense ions, with a 40 s dynamic exclusion and analysed in the linear ion trap. Charge exclusion was set to unassigned, and 1.

2.6. Proteomic data analysis

LC-MS/MS data were initially collected from 5 replicates for each type of alginate microsphere, one saline control and one plasma control. A selection of samples was re-injected into the LC/MS due to some replicates displaying unsatisfactory chromatographic separation (namely, few and broad peaks). Initial data analysis (similar to the one described below) was performed for all collected data, i.e. initial injections and re-injections. This initial analysis culminated in the heatmap of z-scaled label-free quantification (LFQ) values with base 2 of the sample population, Supplementary Fig. S1. Considering the chromatographic quality and grouping of samples, we removed outliers resulting in the following number of replicates for each microsphere fraction: 3 (HG3), 4 (HG4); 4 (SA2), 2 (SA7), 4 (PA1) and 5 (PA7); our analyses and findings are based on these. Preview 2.3.5 (Protein Metrics Inc. https://www.proteinmetrics.com) was used to determine optimal search criteria for the raw files. These parameters were plugged into MaxQuant [53] v 1.5.8.3, which utilises the MaxLFQ algorithm [54] mapping the spectra over Human canonical proteome including isoforms (downloaded in March 2017 [55]). The following search parameters were used: enzyme specified as trypsin with a maximum of 2 missed cleavages allowed, deamidation of asparagine/glutamine, oxidation of methionine, N-terminal acetylation as variable- and carbamidomethylation of cysteine as fixed modification. Mass tolerance for FTMS-MS and ITMS-MS/MS was set to 20 ppm and 0.5 Da, respectively, with false discovery rate (FDR) < 0.01 (high confidence) for peptide spectra matches (PSM), peptide as well as protein group identification. LFQ values for identified protein groups were log-transformed with base 2. Filtered technical replicates were collapsed to their median value, each representing a biological replicate for a set condition. Proteins included in the final dataset were identified by two or more peptides at a fixed FDR protein level of 1.0%. The cut-off for log-transformed LFQ values was set to 16.0 as per the MS-equipment discovered noise-sensitivity level. Proteins assigned with negative PSM scores, identified only by a site, as well as duplicates and known contaminants such as keratins, were removed from the dataset. Protein groups identified in >70% of replicates of at least one group were retained. For the cluster analysis, log₂ LFQ values were z-scaled (except Fig. 1B). The obtained values are relative to the median of the whole expression profile and scaled to variation reflecting relative over- and under-expression. Raw file clustering was based on column-wise z-scaling. The Euclidean distance between the expression vector was used for the hierarchical clustering (http://coxdocs.org/doi ku.php?id=perseususeractivitiesMatrixAnalysisClusteringPCA: HierarchicalCluster) using a k-means algorithm for pre-processing and average linkage for grouping. Median log₂ LFQ intensities representing sample types were presented to Ingenuity® Pathway Analysis (IPA; QIAGEN Inc., https://www.qiagenbioinformatics.com/products/ingenuity-pathway-analysis [56]) to identify top canonical pathways, using an intensity threshold of 16.0. Raw files have been deposited to the ProteomeXchange Consortium [57] via the PRIDE partner repository with the dataset identifier PXD009135 (https://www.ebi.ac.uk/pride/archive/projects/PXD009135) and Notur/NorStore Project NN9036K/NS9036K, respectively.

2.7. Adsorption of plasma proteins to alginate microspheres evaluated by confocal laser scanning microscopy (CLSM)

Alginate microspheres (50 μL) were incubated in pooled (N = 4) lepirudin-plasma (300 μL) for 24 h at 37 °C under rotation and subsequently washed in 0.9% NaCl (2 × 500 μL). Microspheres were stained for complement factors C1q (polyclonal rabbit anti-human C1q/FITC, 50 μg/mL), C3c (polyclonal rabbit anti-human C3c/FITC, 50 μg/mL), or coagulation FXII by unconjugated polyclonal sheep anti-human IgG/CF633 (20 μg/mL). Controls for non-specific antibody binding were polyclonal rabbit-anti-mouse immunoglobulins/FITC (50 μg/mL) and polyclonal donkey anti-sheep anti-IgG/CF633 (20 μg/mL). All incubations were performed for 30 min (37 °C, under rotation) with subsequent washing in 0.9% NaCl (2 × 500 μL). Samples were stored in 0.9% NaCl (200 μL) before analysis and protected from light. Protein deposition was assessed by CLSM (Zeiss LSM 510 Meta, Carl Zeiss Microimaging GmbH, Göttingen, Germany) using a C-Apochromat 10 × /0.45w objective and pinhole of 30.1 μm. 2D images were captured by optical cross-sections through the microsphere equator. 3D images were constructed from sections through the entire microsphere using z-stacks and ImageJ software (National Institutes of Health, New York, USA). An argon laser with an excitation wavelength of 488 nm at 20% laser power, emission over 500–550 nm, and gain 515, were used for FITC-conjugated antibodies. A helium-neon laser with an excitation wavelength of 633 nm at 50% laser power, emission over 650 nm, and gain 530, were used for the CF633-conjugated antibody.

2.8. Complement and coagulation reactivity of microspheres in human whole blood

Initial complement and coagulation responses to microspheres upon blood contact were evaluated using lepirudin-anticoagulated human whole blood, as previously described [44] and with modifications for microspheres [14]. In brief, aliquoted samples of either microspheres (50 μL) in 0.9% NaCl (50 μL) or controls (baseline, PBS [background] and glass) were added 0.9% NaCl (100 μL). All samples were further added PBS with CaCl₂ and MgCl₂ (100 μL). Blood was collected from healthy donors (N = 5) in low-activating polypropylene vials containing the anticoagulant lepirudin (50 μg/mL). Samples were incubated in blood (500 μL) for 4 h (37 °C, continuous rotation), and EDTA was added to a final concentration of 10 mM to inactivate the complement and coagulation responses. For the baseline sample, EDTA-inactivation was performed prior to blood incubation. Samples were centrifuged (4 °C, 1880 × g, 15 min), plasma was harvested and stored at -20 °C before analysis. Complement activation was measured by the enzyme-linked immunosorbent assay (ELISA) kit for detecting soluble TCC. The assay was performed in accordance with the provided protocol. Coagulation activation was assessed by the level of prothrombin cleavage fragment F1 + 2 (PTF1.2) by ELISA kit Enzygnost® F1 + 2, monoclonal. Analysis was performed following the producer’s protocol but included modifications to the plasma dilutions (1:10–1:1000).

2.9. Statistical analyses

In the proteomic analysis, plasma proteins on microspheres were statistically analysed with R [58], using log₂-transformed LFQ values for
group comparisons. For enrichment against the plasma control, a one-sample Student’s T-test [59] was employed with the assumption that the null values were 0. Protein groups missing from all microspheres and identified in the plasma control were categorised as repelled by microspheres with values 0. Values only represented in one group were also set as 0 in subsequent Benjamini-Hochberg corrections [60]. Only protein groups with FDR < 0.1 were considered for further analysis. Protein hydrophobicity and isoelectric points (pI) were calculated using the PepTides software package [61] with the Kyte-Doolittle scale for hydrophobicity and Bjellqvist scale for pI.

For the human whole blood experiment, repeated measures one-way ANOVA with Geisser-Greenhouse correction and Tukey’s multiple comparison test was used to define statistical differences between selected sample groups. Data were log-transformed before analysis due to low sample numbers (N = 5). Differences between sample groups were considered significant at p < 0.05.

2.10. Ethics

The use of blood and plasma from volunteers has been granted by the Regional Ethics Committee of Mid-Norway under REC Central (REK2009/2245), following their recommended guidelines.

3. Results

3.1. Proteomic analysis of human plasma proteins adsorbed to alginate microspheres

Adsorbed plasma proteins were identified by high-resolution LC-MS/MS as outlined in Fig. 1A. Label-free quantification of peptides (E/T-fractions and controls) identified a total of 676 protein groups with relative protein abundances given as log2 LFQ intensity values. Hierarchical clustering of quantified proteins revealed distinct protein adsorption profiles for alginate microspheres HiG, SA, and AP, and the E- and T-fractions thereof (Fig. 1B). Proteins quantified by replicate analysis of each microsphere type invariantly clustered together, indicating high reproducibility of our method. For confident identification of proteins, the initial dataset was further processed using strict conditions: log2 LFQ value cut-off at 16.0, peptide count of at least 2 for identified proteins and the removal of peptides assigned with negative PSM-scores, duplicates and known contaminants. This resulted in a final dataset of 241 confidently identified protein groups (Supplementary Table S1), wherein 236 proteins were identified on the alginate microspheres. In the unfractonated plasma control, 128 proteins were identified and 5 of these proteins were not found on the microspheres. Hence, a total of 113 proteins were exclusively identified on the microspheres and thus enriched above their detection level in unfractonated plasma in our LC-MS/MS setup. A higher number of proteins were identified on microspheres HiG and SA compared to AP: HiG (167 E-/149 T-proteins), SA (182 E-/139 T-proteins) and AP (120 E-/114 T-proteins). As shown in Fig. 1C, several adsorbed plasma proteins were uniquely distributed between the E- and T-fractions. Of the 236 adsorbed proteins, 49 proteins were only identified in the E-fractions and 34 proteins were only identified in the T-fractions. It is reasonable to anticipate that the proteins uniquely identified in the T-fractions represent the proteins that bind most strongly to the microspheres.

3.2. Enrichment of plasma proteins on alginate microspheres

Plasma proteins identified in the current study were assigned their reported concentrations in human plasma using the Peptide Atlas (PA; https://www.proteinatlas.org/humanproteome/blood/proteins+detected+in+ms, accessed Nov. 2021) and the Plasma Proteome Database (PPD; http://www.plasmaproteomedatabase.org, v. 06_2015 retrieved Oct. 2018). The PA (plasma non-glyco 2017 build [62]) presents protein concentrations for 3222 proteins quantified by MS-based plasma proteomics with estimations from spectral counts. The PPD [63] contains published plasma and serum concentrations for 1278 proteins quantified by different methods, wherein plasma protein quantifications by MS spectral counts were only considered. Of the 241 proteins confidently identified in our dataset, plasma concentrations for 198 proteins have been deposited in PA and PPD combined. Proteins that were not reported in the respective databases were mainly immunoglobulin derived. In Fig. 2, the quantified proteins in this study are shown alongside their reported protein concentrations in human plasma. The most abundant proteins (plasma concentrations > 1 µg/mL) were identified both in the plasma control and on the microspheres, whereas less abundant proteins (plasma concentrations < 1 µg/mL) were selectively identified on the microspheres. This suggests that distinct subsets of plasma proteins were significantly enriched on the different alginate microspheres. Among the 113 enriched proteins below the cut-off or not detected in plasma, 32 proteins were exclusively detected in the T-fractions of the microspheres. The plasma concentrations for 25 of these proteins are reported and in the range 0.00029–13.0 µg/mL (PA or PPD), reflecting a high degree of enrichment on the microspheres.

A detailed illustration of the distinct protein adsorption profiles compared to plasma is included in Fig. 3. As shown in Fig. 3A, the protein profiles of the microspheres in terms of relative abundance (log2 LFQ values) were different from that of the plasma control. For the majority of the less abundant proteins in the plasma control, a marked enrichment on the microspheres is evident. Proteins below the cut-off or not detected in plasma and quantified on the microspheres are shown in Fig. 3B. Interestingly, among the proteins that were not detected in plasma, many escaped elution in the first step (E-fraction) but were readily quantified in the T-fractions, indicating strong and selective binding to the distinct microsphere types.

The number of significantly enriched proteins relative to plasma for microspheres HiG, SA, and AP across the E/T-fractions were 106, 128, and 88 proteins, respectively (Fig. 4A). SA had the highest number of uniquely enriched proteins (40), compared to HiG (20) and AP (10). Further information on their binding strengths could be derived from the distribution between E- and T-fractions. Interestingly, two proteins were found to be significantly depleted compared to plasma (not detected in either E- or T-fractions); coagulation factor XIII A chain (F13A1) was depleted on all microspheres, and pregnancy zone protein (PZP) was depleted on AP.

Proteins uniquely identified on either HiG, SA, or AP microspheres were further analysed with respect to their physicochemical properties: hydrophobicity/hydrophilicity and charge/isolectric point (pl) (Fig. 4B). Overall, most of the uniquely adsorbed proteins were hydrophilic in nature (GRASY score below zero). Also, most acidic proteins (i.e. net negative charge at physiological pH) were found in the E-fractions. In contrast, most basic proteins (i.e. net positive charge at physiological pH) were found in the T-fractions. The latter was especially evident for HiG, in which most proteins observed in the T-fraction were basic and could be explained by opposite charge interactions. Much fewer basic proteins were observed for AP, in agreement with the overall charge neutralisation offered by poly-L-lysine. The number of acidic proteins binding to SA was markedly higher than for HiG. This was somewhat surprising since sulfation increases the number of negatively charged groups on the microbeads. However, most of these proteins have previously been reported to bind heparin or heparan sulfate (Fig. 4B, marked by orange circles). This points to a specific role of the sulfate groups in binding these proteins and likely also contributes to the higher number of uniquely identified proteins on SA.

3.3. Different microspheres display distinct adsorption profiles of proteins in the complement and coagulation pathways

The biological relevance of adsorbed plasma proteins was further analysed to elucidate potential immune profiles for the different microspheres. Ingenuity® Pathway Analysis (IPA) is presented in Table 1,
A. **Microspheres incubated in pooled anticoagulated human plasma**

- HiG
- SA
- AP

Plasma incubation 24 h

- 5 replicates/group
- Saline wash 2x
- Removal of unbound proteins
- Saline (SC) Plasma (PC)

B. **Two-step isolation of adsorbed and bound proteins**

- Elution of proteins
- On-microsphere tryptic digestion
- Trypsin
- Desalting using C18 stage tip column
- Tryptic peptides in solution

C. **Proteomic analysis by high resolution LC-MS/MS (Orbitrap)**

- Replicate sample analysis
- Reanalysis and removal of selected replicates (poor chromatographic separation)

- Data analysis using MaxQuant - Perseus
- Protein identification and quantification
- Search: Uniprot Human Proteome

- Raw dataset
- 676 protein assignments
- Data reduction
- 236 adsorbed proteins (241 total)

- In-depth analysis of differentially adsorbed proteins

D. **Confident identification of adsorbed proteins**

- 236 proteins

- E
- T
- HiG
- SA
- AP

- 49
- 153
- 34

(caption on next page)
showing the ten most abundant proteins and top canonical pathways identified for the microspheres. The most abundant protein of the plasma control was albumin (ALB), which was also ranked the highest for HiG and AP, but not for SA (ranked third). Besides ALB, protein abundances on the microspheres did not correspond to the unfraccionated plasma control, again highlighting the specific protein adsorption to the microspheres. IPA further revealed the top canonical pathways assigned to the relevant proteins, signifying the immune processes ([68,69]) and complement activation (Table 1). Significant enrichment was observed for the C1 complex (complement C1q with its associated proteases C1r and C1s), involved in the initialisation of the classical pathway. C1q comprises subunits C1QA, C1QB and C1QC, which were 152-197-fold enriched on HiG (values given relative to plasma control), 13-140-fold on SA and 2-9-fold on AP, whereas the proteases (C1R, C1S) were only enriched on HiG (17-27-fold) and SA (65-122-fold). In agreement with this, the level of C1q surface-recruiting protein serum amyloid P-component (APCS) was highly pronounced on HiG (>193-fold) and SA (>230-fold), as well as lower-level enrichment of immunoglobulin G1 (IGHG1) and C-reactive protein (CRP). AP had the highest enrichment of CRP, being >3-fold above the other microbeads. The proteins comprising the classical C3 convertase (C4B, C2 [A]), which is activated by the C1 complex, were more prominent on HiG and SA. Proteins of the lectin pathway, including mannose-binding protein C (MBL2), ficolin-2 (FCN2), collectin-11 (COLEC11) and mannann-binding lectin serine protease 1 (MASP1), were also identified on HiG and/or SA but below the detection level in the plasma control. In addition to activators of the classical and lectin pathways, we observed selective enrichment of inhibitors for these pathways on HiG and SA. Plasma protease C1 inhibitor (C1INH), which inhibits the C1 complex and MASPs, respectively, was enriched on SA (7-fold) and HiG (2-fold). C4-binding protein (C4BPA/C4BPB complex), an inhibitor of the classical pathway, was exclusively enriched on SA (>2-fold). The selective enrichment of proteins from the alternative pathway was, however, not as evident on HiG and SA as compared to AP. This pathway is the main driving force of terminal complement activity, involving complement component 3 (C3) and complement factors B (CFB), D (CFD) and properdin (CFP). C3 plays a central role in complement activation, acting as a point of convergence for all three pathways and fuelling the amplification process. CFB and CFD both contribute to the activity of C3. CFP can serve as a local initiator of the pathway by recruiting C3 to the surface and also plays a vital role in stabilising the alternative C3 convertase. AP had the highest enrichment of C3 and CFP, roughly 5-fold above HiG and SA. Notably, CFP was not detected in plasma and was exclusively enriched in the T-fractions, indicating strong binding. Crucial inhibitors of C3 activity include complement factor H (CFH) and I (CFI). CFH was significantly enriched on SA (>44-fold) and to some extent on HiG (>2-fold), while below the plasma control for AP. CFI was enriched (>2-fold) on all microspheres. Component components of the terminal complex (TCC, C5, C6, C7, C8, C9) were enriched (2-59-fold) on all microspheres. Inhibitors of TCC assembly, including clusterin (CLU) and vitronectin (VTN), were most pronounced on SA (CLU: ~40-fold, VTN: ~6-fold). Carboxypeptidase-N (CPN; CPN1/CPN2), which degrades anaphylatoxins (C3a, C5a), was exclusively distinguished (catalytic subunit CPN1) on SA.

The coagulation protein profiles are summarised in Fig. 5B. Proteins of the contact activation (intrinsically) pathway [70], including plasma kallikrein (KLKB1), kininogen-1 (KNG1), coagulation factors XII (F12), XI (F11) and IX (F9), were all enriched on the microspheres and especially evident on SA. Here F12, which initiates the pathway, was enriched >64-fold on SA compared to >3-fold and >4-fold on HiG and AP, respectively. Proteins of the tissue factor (extrinsic) pathway, including factor III (F3) and VII (F7), were not detected in the dataset. The common coagulation proteins, factors X (F10) and V (F5), were distinct for SA and HiG. Vitamin K-dependent protein C (PROC) that functions as an anti-coagulant when activated, including its cofactor vitamin K-dependent protein S (PROS1), were particularly enriched on SA. As part of the clotting process, prothrombin (factor II) is proteolytically cleaved to form thrombin (factor IIa) that converts fibrinogen into fibrin. Prothrombin/thrombin (F2) was most enriched on AP (>5-fold), followed by HiG (2-fold) and SA (<2-fold). Inhibitors of thrombin include antithrombin-III (AT3), which inhibits several coagulation factors, and heparin cofactor 2 (HCFG2). Notably, SA showed the highest enrichment of AT3 (>12-fold) and HCF2 (4-fold). Plasmin is generated from the zymogen plasminogen on the surface of fibrin clots as part of the fibrinolytic system, which has also been implicated in complement-independent cleavage of C5 and C3 [69]. Plasminogen/plasmin (PLG) was exclusively enriched in the T-fraction of AP (4-fold).

Fig. 5C displays adsorbed proteins with various biological functions that may be relevant to the PFO outcomes of the microspheres. These proteins include extracellular matrix (ECM)-associated proteins, apolipoproteins, monocyte-associated proteins and cytokines or chemo-attractants. For the ECM proteins, ECM protein 1 (ECM1) was extensively enriched on SA (>170-fold) and to some extent on HiG (7-fold), and tenasin-X (TNXB) was distinctively identified on SA. Further, the ECM degrading proteins: matrix metalloproteinase-2 (MMP2) and -9 (MMP9) and neutrophil elastase (ELANE; Table S1) were highly enriched and unique for SA. The tissue inhibitors of metalloproteinase 1 (TIMP1) and 2 (TIMP2), which regulate the MMPs, were exclusively enriched on SA and HiG. Several apolipoproteins (not all shown; see Table S1 for full list of proteins) were either unique or most enriched on SA, including apolipoprotein E (APOE) and H (APOH). Proteins involved in monocyte activation, by lipopolysaccharide (LPS) include the LPS-binding protein (LBP) and monocyte differentiation antigen CD14, which were enriched on all three microspheres. The pro-inflammatory cytokines, including platelet factor 4 (PF4), PF4 variant 1 (PF4V1) and leukocyte cell-derived chemotaxin-2 (LECT2), and the chemoattractant azurocidin (AZU1), were enriched above the detection level in plasma and consistently more pronounced or exclusive for HiG and AP.

A selection of the identified proteins is presented in a heatmap (Fig. 5D), showing the relative protein abundances between the three types of microspheres across the E- and T-fractions. Samples from each type of microsphere formed distinct clusters, and the largest dissimilarity
Fig. 2. Human plasma proteins identified in this study ranked according to their reported plasma protein concentrations retrieved from the Peptide Atlas [62] and Plasma Proteome Database [63]. Proteins quantified in the unfractionated plasma control are presented as orange bars (upper axis) and reported plasma protein concentrations are indicated by dots (lower axis) according to their distinct detection: microspheres* (black), on-microsphere trypsinated (T)-fractions (blue), plasma control (yellow), and both on microspheres and in plasma control (red). In the current work, a total of 241 plasma proteins were confidently identified, of which 198 proteins were reported with plasma concentrations determined by MS spectral counts. Proteins are denoted by gene names.*Proteins identified in either eluted (E) or E- and T-fractions.
Fig. 3. Enrichment of plasma proteins on alginate microspheres after incubation in human lepirudin-plasma (24 h). Protein abundances, represented as log₂ LFQ values, for 241 proteins identified for the microspheres (HiG, SA, AP) and unfractionated plasma control. Microsphere samples comprised separate fractions of eluted (E) and on-microsphere trypsinated (T) proteins. (A) Quantified proteins in the plasma control ranked according to their detection level (descending order), including the respective protein profiles of the microspheres. (B) Enriched proteins on the microspheres, which were below the cut-off or not detected in the plasma control. Proteins are denoted by gene names.
The deposition of complement and coagulation proteins on the microspheres was studied by CLSM, and functional responses were assessed in a human whole blood assay (Fig. 6). The binding of C1q was distinct between HiG and AP, respectively. Whereas no significant TCC induction was observed for SA, low induction was observed for HiG (p < 0.01) and a strong induction for AP (p < 0.001) compared to baseline (Fig. 6E). The saline control for TCC (not shown) was significantly elevated (p < 0.01) compared to baseline (Fig. 6F). The PTF1.2-response for SA as well as for the positive control (glass, not shown) were also significantly (p < 0.01) elevated above the saline control (not shown).

A graphical summary of proposed complement and coagulation mechanisms for the three types of alginate microspheres is presented in Fig. 7, with a basis on elucidated proteomic immune profiles (Fig. 5) and functional data on complement and coagulation reactivity (Fig. 6). Details are outlined in the figure legend.

4. Discussion

Here, we use high-resolution LC-MS/MS to identify distinct protein adsorption profiles for three types of alginate microspheres relevant for immune isolation in cell therapy, which we recently reported exhibit different inflammatory and PFO responses: HiG (low-inflammatory and fibrictic), SA (low-inflammatory and anti-fibrictic), and AP (pro-inflammatory and highly fibrictic) [10]. A total of 236 proteins were differentially adsorbed to the microspheres, and in-depth analyses of the proteins revealed unique immune profiles. In detail, the microspheres showed differences in enriched complement and coagulation factors with inhibitory or activating roles. Of specific importance is the prominent enrichment of inhibitors of complement and coagulation on SA, coinciding with minimal PFO. These findings were supported by functional assessments in human whole blood (hWB) involving total complement and coagulation activation. The current work establishes MS-based quantitative proteomics as a valuable tool, in conjunction with established in vitro and in vivo methods, to identify potential drivers of inflammation and PFO for alginate-based hydrogels. In the following, we discuss our methodological strategy and the effect of hydrophobicity/hydrophilicity and charge/isoelectric point. Further, we include an in-depth discussion of specific proteins involved in the complement and coagulation cascades that were prominent in the canonical pathway analysis, as well as other proteins that may be relevant in PFO development.

The competitive displacement of adhering surface proteins by other proteins with higher binding affinities is commonly referred to as the Vroman effect [37,75]. Consequently, the protein adsorption behaviour of a material depends on the composition of the protein solution and the exposure time. In the current study, we chose a strategy that preserved the reactive complement proteins and coagulation factors in human plasma, which sets an important premise for the subsequent protein displacements. To distinguish between weaker and stronger bound proteins, we chose to employ a two-step detachment procedure (primary
elution [E] and secondly on-microsphere trypsinisation [T]). The T-fraction represents the proteins with the overall strongest binding, which is supported by the many proteins below the detection level in plasma selectively identified in the T-fraction. The highly abundant plasma proteins were predominantly identified in the E-fraction. The enrichment of proteins from plasma was evident for all the studied microspheres. However, the number of different proteins was highest on the anti-fibrotic SA and lowest on the pro-fibrotic AP. This indicates that the number of proteins by itself is not a driver of the host response, but rather the type of proteins and their capability to react with the material surface, as will be discussed in later sections.

Hydrogels constitute a unique class of hydrophilic materials, comprising water-swollen networks of hydrophilic polymers. Their protein adsorption behaviour is thus not directly comparable to that of other non-hydrogel hydrophilic materials, such as functionalised solid surfaces that are more widely described in the literature ([76] and references therein). The three types of hydrogel microspheres in this study primarily differ in their functional groups, which also dictate the surface charge. The alginate (present in all the microspheres) is negatively charged at physiological pH due to the presence of carboxylate groups (-COO⁻), while the sulfated alginate (in SA) carries additional negative charges ([24]. Complexation of the alginate hydrogel with poly-L-lysine (PLL; AP), proteins were predominantly identified in the E-fraction. The enrichment of proteins from plasma was evident for all the studied microspheres. However, the number of different proteins was highest on the anti-fibrotic SA and lowest on the pro-fibrotic AP. This indicates that the number of proteins by itself is not a driver of the host response, but rather the type of proteins and their capability to react with the material surface, as will be discussed in later sections.

Hydrogels constitute a unique class of hydrophilic materials, comprising water-swollen networks of hydrophilic polymers. Their protein adsorption behaviour is thus not directly comparable to that of other non-hydrogel hydrophilic materials, such as functionalised solid surfaces that are more widely described in the literature ([76] and references therein). The three types of hydrogel microspheres in this study primarily differ in their functional groups, which also dictate the surface charge. The alginate (present in all the microspheres) is negatively charged at physiological pH due to the presence of carboxylate groups (-COO⁻), while the sulfated alginate (in SA) carries additional negative charges ([24]. Complexation of the alginate hydrogel with poly-L-lysine (PLL; AP), which contains positively charged amino groups (-NH₂) at physiological pH, decreases the net negative charge at the capsule surface of AP [5].

The number of significantly enriched proteins increased with the negative charge of the microspheres (SA > HiG > AP) (Fig. 4A), pointing to charge interactions as important drivers for the observed protein binding. There was a trend towards a more positive charge of the proteins in the T-fraction, supporting that opposing charge interactions play an important role in promoting the strongest binding to the microspheres. The high number of negatively charged proteins uniquely binding to the microspheres may be explained by positively charged surface patches that could dictate their binding despite an overall net negative charge [38]. One such example is the known sugar-binder inter-alpha-trypsin inhibitor heavy chain 1 (ITIH1). This protein contains a positively charged lysine cluster aligned on top of a β-sheet on the protein surface (PDB: 6FPY) [77], which might explain the strong association to HiG. The inclusion of sulfated alginate in the alginate microbeads (SA) resulted in an overall increase in adsorbed proteins as well as uniquely enriched proteins in the E-fraction. Notably, the majority (>63%) of the negatively charged proteins binding to SA have previously been reported to bind heparin and/or heparan sulfate [64-67]. Heparin and heparan sulfate are sulfated glycosaminoglycans (GAGs) that interact with a wide range of proteins in the regulation of different biological processes such as the immune response or response to wounding [64]. The structure-function properties of sulfated alginate have been associated with those of heparin and heparan sulfate [24,78], and sulfated alginate has previously been shown to bind several heparin-binding proteins [24,26].

Alginate hydrogels have water-swollen, porous structures (~2% w/v polymer concentration) that could allow proteins to penetrate below the microsphere surface [79]. Coating alginate microbeads with PLL decreases the pore size of the microspheres [80], which could contribute to the lower number of proteins on AP. Previous studies on the surface topography of alginate microspheres using atomic force microscopy (AFM) revealed similar average surface roughness for Ca- or Ba-alginate microbeads and alginate-PLL-alginate microspheres [81]. In a recent AFM study, we showed that the inclusion of oxidized alginate in soft alginate hydrogels leads to an increase in surface roughness [82]. Like oxidized alginate, sulfated alginate also contributes poorly to the ionic network of the hydrogel [83,84]. Thus, higher surface roughness could potentially be expected for SA when compared to HiG. However, the effect of topography as a driver for protein adsorption in the studied microspheres remains elusive.

Complement is considered a key contributor to biomaterial-induced host responses [41]. The coagulation cascade may influence the host response by direct activation through the contact pathway or through cross-talk with the complement system [71]. Ingenuity pathway analysis (IPA) identified the acute-phase response and the complement and coagulation cascades as the top enriched canonical pathways for all three microspheres. However, the protein adsorption does not necessarily reflect a biological response, since the acute-phase effectors which include most of the complement and coagulation proteins depend on distinct conformational changes to elicit their biological functions [41,85]. Thus, we interpret the proteomics data (Fig. 5) alongside the functional data in hWB with assessments of total complement and coagulation activation (Fig. 6). In agreement with our findings, initial in vivo adsorption of acute-phase proteins was also reported for fibrotic PEG hydrogels explanted from mice [27]. This supports the significance of active proteolytic cascades in the early phases of the host response and fibrotic tissue development, as well as the relevance of using leupirudin plasma in vitro.

In brief, the complement system consists of an intricate network of effectors and regulators. Driven by conformational changes, complement activation could be initiated through the alternative, classical, or lectin pathways. This culminates in the formation of convertases, which in turn generate the complement effectors, including opsonins (e.g. C1q, C3b), anaphylatoxins (e.g. C3a, C5a), and terminal complement complex (TCC) [68,69]. The potent biological effects of these effectors are tightly regulated by inhibitors, consisting of cellular receptors or soluble humoral factors that also bind to GAGs on cell surfaces [68,86,87]. In the current study, SA showed insignificant terminal complement activation (TCC formation) in hWB, which represents the functional endpoint of complement activation. This conforms with the enrichment of complement inhibitors in the proteomic analysis, including C1 inhibitor (C1IN), factor H (CFH), C4-binding protein (C4BP), clusterin (CLU), vitronectin (VTN), and carboxypeptidase-N (CPN). Interestingly, the catalytic subunit of CPN, which serves to mitigate the pro-inflammatory, chemotactic signalling of the anaphylatoxins C3α and C5a [69], was exclusively enriched on SA. The abundant enrichment of CFH on SA is intriguing as it is involved in the inhibition of complement at the level of C3. It is acknowledged that CFH can bind directly to polyansions such as sulfated GAGs and sialic acid on host cells [85]. It has also been demonstrated that C1IN directly binds to heparin [88] which exhibits properties similar to sulfated alginate. The enrichment of complement inhibitors to SA (containing sulfated alginate) is likely biologically significant, as shown by the low TCC response and could at least partly be related to a direct binding of these factors. In addition, low levels of C3 in both proteins (enriched >2-fold from plasma) and CLSM analyses, together with a pronounced enrichment of CFH (~44-fold) for SA, indicates that the balance of activating and inhibiting proteins is important for the biological outcome. This is further apparent when comparing to AP, which showed low levels of the complement inhibitors while the highest deposition of C3 and properdin (CFP). This further coincides with a significant TCC response in hWB. The abundant plasma protein C3 is crucial for downstream complement activation, where CFP serves to...
Fig. 5. Immune profiling of adsorbed plasma proteins on alginate microspheres. Isolated proteins from eluted (E)- and trypsinated-on-microsphere (T)-fractions of the microspheres (HiG, SA, AP) and the plasma control. (A) Adsorbed proteins of the complement system, (B) coagulation system, and (C) other potentially relevant proteins grouped with their associated pathway or mechanistic function. Protein abundance is given as log2 LFQ values, where a difference of 1 equals a 2-fold change. (D) Selected adsorbed plasma proteins are presented in the heatmap using z-scored log2 LFQ values. The median score is zero (black), and the grey colour indicates not detected proteins. Proteins are denoted by gene names. TCC = terminal complement complex, FL = fibrinolytic system, Matrix = extracellular matrix-associated, Apo = apolipoproteins, Mono = monocyte associated, CTX = chemoattractant.
Fig. 6. Evaluation of complement and coagulation proteins and responses on/to alginate microspheres. Detection of complement (C1q, C3c) and coagulation proteins (FXII) in human plasma by CLSM (A-D) and activation in human whole blood by terminal complement complex (TCC) and prothrombin fragment 1 + 2 (PTF1.2) (E, F). CLSM images show antibody-stained alginate microspheres HiG, SA, and AP after incubation (24 h) in lepirudin-anticoagulated human plasma. Microspheres were FITC-stained (green) against complement C1q (A) and C3c (B) and CF633-stained (red) against coagulation FXII (C), and non-specific antibody binding was assessed (D). Captured images include brightfield (BF), equatorial (2D)-sections and (3D)-projections of z-stacked images. Scale bar: 200 μm. Activation of complement by TCC-induction (E) and coagulation by PTF1.2 formation (F) was assessed after incubation (4 h) in lepirudin-anticoagulated human whole blood. Controls measured (median ± SEM), but not shown, included positive control for PTF1.2 (glass): 759 954 ± 197 581 pmol/L, and saline control: 12.9 ± 5.2 AU/mL (TCC) and 401 ± 169 pmol/L (PTF1.2). Data are expressed in box plots with values from five donors. Significant values are given as \( p \leq 0.05 \) (*), \( p \leq 0.01 \) (**), \( p \leq 0.001 \) (***) between indicated sample groups. T0 represents the experimental baseline. (For interpretation of the references to colour in this figure legend, the reader is referred to the Web version of this article.)
distinct in the absence or low levels of initial complement inhibitors. This is in accordance with a persisting complement response and subsequent terminal com-
prothrombin/thrombin (FII [α]) and plasminogen/plasmin (PLG) also present the additional possibility of a complement-independent activation of C3 and C5. AP is enriched with fewer inhibitors (C1IN, CFH, CFI, CLU, VTN). HIG is enriched with with inhibitors (C1IN, CFH, CFI, CLU) and to a lesser extent. HIG, and especially SA, exhibit low terminal complement activity (fluid-phase TCC; sTCC) in hWB, despite being enriched with proteins involved in TCC formation, which suggest inactivation of TCC or adsorption of non-assembled TCC-components. AP displays pronounced enrichment of CFP and C3, indicating complement initiation and propagation through the alternative pathway. Moreover, enrichment of prothrombin/thrombin (FII [α]) and plasminogen/plasmin (PLG) also present the additional possibility of a complement-independent activation of C3 and C5. AP is distinct in the absence or low levels of initial complement inhibitors. This is in accordance with a persisting complement response and subsequent terminal complement activity, shown for these microspheres by the high levels of adsorbed proteins involved in TCC formation and the significant TCC response in hWB. The coagulation system is activated through two mechanisms: the extrinsic (tissue factor) pathway (not discussed here) and the intrinsic (contact activation) pathway, which has been described elsewhere [70,72-74]. All the microspheres activate coagulation to some extent, as seen by the functional hWB data. SA has an overall moderate coagulation reactivity but the highest coagulation (prothrombin fragment 1 + 2) response among the microspheres. Being highly enriched with proteins of the intrinsic pathway, such as FXII, suggests coagulation activation through the contact system. SA is also enriched with numerous coagulation inhibitors (AT3, HCF2, C1IN, PROC, ZPI), which likely diminishes this activation. HIG shares a similar coagulation profile to SA in types of enriched proteins, although at significantly lower abundances and with some variation in adsorbed inhibitors (i.e. PROC, TFF). Distinctively, AP is enriched with all the contact system proteins, except for C1IN, which potentially allows for pro-inflammatory signalling by BK. Further enrichments include several coagulation inhibitors (AT3, HCF2, PROC, ZPI, TFF). AP shows the highest enrichment of FII(α) yet distinctly lacks central proteins (FX, FV) of the intrinsic pathway. Hence, the observed coagulation reactivity in hWB indicates tissue factor-dependent initiation [48], closely linked to complement activation.

stabilise the C3 protein in its active form (C3 convertase) [68]. Thus, the data indicates that the C3 convertase is built at the surface of AP, with further downstream activation of the complement cascade leading to the formation of TCC. Previously, we have shown that the binding of C3 to the surface of AP leads to the adhesion of leukocytes in vitro with subsequent secretion of pro-inflammatory cytokines [15,16]. In agreement with our previous work, the proteomics study by Wang et al. on human serum proteins adsorbed to PEG hydrogels revealed the binding and activation of C3, where the inactivation of C3 (incubation in C3-inactivated serum) led to a reduction in the attachment of human monocytes in vitro [20].

In the functional assay (hWB) herein, HIG induced a low TCC response yet significantly elevated above that of SA. The proteomic analysis may provide insight into the subtle differences in inflammatory potentials of the microspheres, showing that the enriched complement inhibitors were significantly less abundant on HIG compared to SA (Fig. 7). Intriguingly, both microspheres showed an extensive enrichment of C1q (classical pathway), as well as being enriched with proteins of the lectin pathway, which could indicate an initial complement recognition. However, if this recognition leads to complement activation it is likely subdued at an early stage, in accordance with enriched inhibitors (C1IN), lower-level enrichment of C3, minimal C3c deposition verified by CLSM and, importantly, low TCC induction in the functional hWB assay. In support, the cluster analysis of bound proteins showed a potential inac-
tivation of C1 complex (C1q/C1r/C1s) by grouping its inhibitor (C1IN) with the C1q-associated proteases (C1r, C1s). C1IN is known to bind these proteases, forming an inactive covalent complex that dissociates from C1q and hinders downstream complement activation [69]. Interest-
ingly, C1q was more enriched on HIG whereas C1IN was more enriched on SA, which might explain the slightly lower complement activation of SA in hWB. It has previously been shown that sulfated polysaccharides (e.g. sulfated GAGs and dextran sulfate) potentiate C1IN activity [89]. The anti-inflammatory effects of C1IN encompass the regulation of the classical and lectin complement pathways, as well as the coagulation (contact pathway) and fibrinolytic systems [86].

In the assessment of the total coagulation activation in hWB (pro-
trombin factor 1 + 2; PTF1.2), we found an elevated response for SA. The proteomics data showed a marked enrichment of the initiators of the contact pathway on SA, including coagulation factor XII (FXII), plasma kallikrein (KLKB1) and high-molecular-weight kininogen (KNG1), thus pointing to an initiation through the contact pathway. Still, the coagulation response of SA is considered moderate in comparison to the glass control, which is a prominent activator of FXII [48]. This could be explained by the enrichment of C1IN, which also regulates the contact pathway. In addition, SA was enriched with several coagulation inhibitors, especially antithrombin-III (AT3) and heparin cofactor 2 (HCF2). This finding points to a similarity to heparin that mediates its anticoagulation effect through the binding of AT3 [90].

In the following sections, we discuss the proteomics data in connec-
tion with the previously reported PFO outcomes and focus on the poorly understood differences in PFO between HIG and SA, the former being prone to PFO as opposed to the latter exhibiting minimal PFO in vivo [10]. Their elucidated immune profiles present similar protein identities, except for a few regulatory proteins, yet they display distinct protein abundances. These subtle differences might tip the balance toward a PFO response as seen for HIG. In detail, SA was unique in its abundant and strong association to a multitude of complement inhibitors, which were less prominent on HIG. Importantly, this includes the binding of compo-
mlement factor H (CFH) that was profoundly more enriched on SA compared to HIG and, contrastingly, not enriched on AP. The abundant enrichment of CFH is particularly interesting as it serves a protective role against complement-targeted destruction in the host [68], and CFH enrichment strategies have previously been used to improve the biocompatibility of biomaterials [91]. In addition, an extensive enrich-
ment of serum amyloid-P component (APCS) was found on HIG and SA. APCS is involved in several aspects of innate immunity, including inhibiting the differentiation of fibrocytes and pro-fibrotic macrophages, and has been proposed as a potential anti-fibrotic therapeutic [92]. The strong binding of IgG (e.g. IGHG1) and other immunoglobulins was consistently more pronounced on HIG. The classical pathway, mediated by the action of C1q and its numerous pattern recognition molecules, is strongly initiated by IgG or IgM [68]. Cluster analysis of the proteomics data grouped IgG with C1q (Fig. 5D), which was most prominent for SA and could point to a relatively larger degree of C1q inactivation. Thus, the potential activation state of C1q might prove relevant for the PFO outcomes of HIG (fibrotic) and SA (anti-
fibrotic). Complement proteins (such as C3) play a central role in fibrotic tissue development [17,19], and we recently demonstrated the in vivo deposition of C3 on highly PFO-prone AP microspheres [10]. In the proteomics study herein, AP displayed the highest enrichment of C3 and, intriguingly, the acute-phase protein C-reactive protein (CRP). CRP is involved in classical complement activation [68] and has further been shown to promote cell-mediated responses with potential recruitment of inflammatory cells [93]. Romero-Gavilan et al. found that CRP, as well as C1q, was most abundant on titanium-based implants that were prone to fibrotic responses, wherein the authors postulate that the ratio of complement activators and inhibitors may determine the in vivo outcome [30].
The fibrinolytic system is known to restrict the propagation of blood clots by dissolving fibrin during wound healing processes. In our previous in vivo experiments [10], the accumulation of fibrinogen on the microspheres was found to coincide with PFO, where SA exhibited a significantly lower degree of PFO and fibrinogen deposition than HiG and AP. In the current study, specific regulatory factors of fibrinolysis [94], involving the activation of plasminogen to form the active fibrinolytic enzyme plasmin, could indicate that SA has a higher inherent potential for fibrinolysis. The levels of the plasminogen activators FXII and KLKB1 were markedly higher on SA, and the plasmin inhibitor alpha-2-macroglobulin (A2M) was strikingly more depleted, compared to HiG and AP (Supplementary Fig. S2).

The significantly enriched heparin-binding proteins which were unique for the anti-fibrotic SA include the matrix metalloproteinases (MMPs [MMP2, MMP9]), neutrophil elastase (ELANE) and tenasin-X (TNXB). The ECM degrading enzymes MMP2 and MMP9 have been found to inhibit, and also promote, fibrosis in different fibrotic disease models [95,96]. Interestingly, the MMPs and their regulators (TIMPs) were enriched on SA, while only the latter was enriched on HiG. The intricate balance between MMPs and TIMPs and their potential roles in fibrosis might prove relevant for biomaterial-mediated fibrotic responses and, in effect, the fibrotic outcome for SA and HiG. The neutrophil-derived protease ELANE modulates innate immunity and inflammation, where excessive activity has been shown to hamper phagocytic recognition and clearance through the digestion of opsonins and opsonin receptors [97]. The ECM glycoprotein TNXB plays an important role in ECM architecture and tissue integrity, which has been shown to have anti-adhesive properties [98]. Several apolipoproteins involved in lipid metabolism, among others [99], were detected on the microspheres, which were consistently more pronounced on SA compared to HiG and AP. Interestingly, the apolipoproteins E (APOE) and H (APOH; β2-glycoprotein 1) have been reported to have anti-fibrotic effects [100,101].

In summary, the previous sections have highlighted proteins that may have an impact on the PFO responses seen in vivo [10], with a particular focus on HiG and SA. Sulfated alginate reduces the fibrotic host response towards empty and cell-containing microbeads compared to high G alginate [3,10], demonstrating the significance of using biomaterials with low inflammatory potential in cellular therapies that depend on the free diffusion of oxygen and nutrients to encapsulated cells. In this study, the binding of inhibitors (e.g. C1IN and CFH) and heparin-binding proteins to SA are striking. Recruiting CFH to biomaterial surfaces has previously been shown to attenuate biomaterial-mediated inflammatory responses [91], thus underscoring the clinical relevance of surface-associating proteins in terms of biocompatibility. Importantly, as the proteomic analysis does not provide information on the activation state of the proteins, it needs to be supported with functional studies. Here, we focused on the proteolytically active cascades of complement and coagulation in human whole blood. The proteomics data serves to deepen our understanding of the mechanisms of activation by providing insight into the binding of activators and inhibitors to the biomaterial surface. This culminates in the biological effects seen as complement or coagulation activation in vitro or fibrotic tissue development in vivo.

5. Conclusion

The current study is the first to document the adsorption of human plasma proteins on alginate hydrogel microspheres using LC-MS/MS-based proteomics. In conjunction with functional data of complement and coagulation activation in human whole blood, the proteomic analysis signifies a physiologically relevant method for elucidating protein-based immune profiles of alginate hydrogel materials. Utilising lepirudin-based plasma enables the investigation of proteolytic activable cascades of the complement and coagulation systems, which are critical activators of the host immune system. Protein profiling revealed novel details on the selective protein binding to the different alginate-based materials, and that could help explain their different PFO outcomes shown in previous studies. The abundant binding of complement and coagulation inhibitors to SA conforms to a low-inflammatory and anti-fibrotic profile. Moderate levels of inhibitors to HiG conform to a low-inflammatory but pro-fibrotic profile. In contrast, the enrichment of complement activators in combination with low amounts of inhibitors on AP conforms to a pro-inflammatory and pro-fibrotic profile. The current work presents a step forward in understanding the underlying mechanisms of the inflammatory and PFO responses towards alginate-based microspheres. SA possibly evades fibrosis through the extensive binding of acute-phase inhibitors. Heparin-binding proteins enriched on SA may have additional anti-fibrotic effects. Ultimately, the method and results presented in this study can serve as tools to tailor novel biocompatible alginate materials intended for cell-based therapies as well as other therapeutic or diagnostic applications.

Credit author statement

Abba E. Coron: Conceptualisation, Methodology, Validation, Formal analysis, Investigation, Writing – original draft, Writing – review & editing, Visualisation. Davi M. Fonseca: Conceptualisation, Methodology, Validation, Investigation, Writing – review & editing. Animesh Sharma: Conceptualisation, Methodology, Validation, Formal analysis, Resources, Writing – review & editing. Geir Slupphaug: Conceptualisation, Methodology, Validation, Resources, Writing – review & editing, Funding acquisition. Berit L. Strand: Conceptualisation, Methodology, Validation, Resources, Writing – review & editing, Supervision, Project administration, Funding acquisition. Anne Mari A. Rokstad: Conceptualisation, Methodology, Validation, Resources, Writing – review & editing, Supervision, Project administration, Funding acquisition.

Funding

This work was supported by the Norwegian University of Science and Technology (NTNU), Faculty for Natural Science, The Liaison Committee for Education, Research, and Innovation in Central Norway (Regional Health Authority, Samarbeidsorganet) under grant 46056819, CEMIR NFR grant 223255, NTNU Health project “Tailored biomaterials with reduced immune responses”, and the Chicago Diabetes Project (www.chicagodiabetesproject.org). PROMEC is funded by the Faculty of Medicine at NTNU and Central Norway Regional Health Authority. PROMEC is a member of the National Network of Advanced Proteomics Infrastructure (NAPI), which is funded by the RCN INFRASTRUKTUR-program (295910).

Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Data availability

Data will be made available on request.

Acknowledgements

We thank professor emeritus Gudmund Skjåk-Bræk, NTNU, for support on the development of sulfated alginate as well as on previous work on alginate microspheres. Professor Jose Oberholzer, University of Virginia, is acknowledged for continuous support in the development of encapsulation systems for type 1 diabetes. Øystein Arlov at the SINTEF research institute is credited for providing guidance in the sulfation of alginate and measuring the sulfur content (HR-ICP-MS) of the sulfated alginate.
Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.mtbbio.2022.100490.

References

[1] D. Jacobs-Tulleners-Thevison, M. Chintinne, Z. Ling, P. Gillard, L. Schoonjans, G. Delvaux, B.L. Strand, F. Gorus, B. Keymeulen, D. Pipériers, Sustained function of alginate-encapsulated human islet cells in the peritumoral cavity of mice leading to a pilot study in a type 1 diabetic patient, Diabetesologia 56 (7) (2013) 1605–1614.

[2] M.A. Roelapsed, O. Veiseh, A.J. Vegas, J.C. Doloff, M.A. Bochenek, A.J. Vegas, J. Li, A.R. Bader, J. Li, L. Gazda, P. Thompson, L.R. Badell, A. Sambanis, C. Ricordi, C.J. Weber, Microencapsulated adult porcine islets transplanted intraperitoneally in streptozotocin-diabetic non-human primates, Transplantation 2025 (2018), e12450.

[3] Q. Liu, A. Chiu, L.H. Wang, D. An, M. Zhong, A.M. Smink, B.J. de Haan, P. de Vos, K. Keane, A. Vegge, E.Y. Chen, W. Song, W.F. Liu, J. Flanders, C. Rescan, L.G. Grunnet, X. Wang, M. Ma, Zwitterionically modified alginites mitigate cellular overgrowth for cell encapsulation, Nat. Commun. 10 (1) (2019) 5262.

[4] A.J. Vegas, O. Veiseh, J.C. Doloff, M.A. Roelapsed, K.S. Hoem, A.E. Coron, G. Skjåk-Bræk, O.-L. Brekke, J. Hollister-Lock, T. Ekdahl, K.S. Hoem, A.E. Coron, G. Skjåk-Bræk, Heparin-Like properties of sulfated alginites with defined sequences and sulfation degrees, Biomacromolecules 15 (7) (2014) 2744–2750.

[5] A. Lovrol, F.L. Anchmann, A. Sundan, T. Espevik, G. Skjåk-Bræk, Heparin-Like properties of sulfated alginites with defined sequences and sulfation degrees, Biomacromolecules 15 (7) (2014) 2744–2750.

[6] J. Ma, S. Yang, S. Mostly, T. Truscott, E. Buck, L. Lee, P. Ong, L. Song, W. Zhang, B. Luster, A. Exton, F. Elortza, M. Gurruchaga, I. Go, M. Gurruchaga, I. Go, A. Chiu, S. Siebert, K. Tang, A. Chiu, S. Siebert, K. Tang, M. Qi, J. McGarrigle, R. Langer, D.G. Anderson, Combinatorial hydrogel library enables identification of materials that mitigate the foreign body response in primates, Nat. Biotechnol. 34 (3) (2016) 345–352.

[7] A. Alrouk, J.M. Anderson, D.T. Chang, Foreign body reaction to biomaterials, Drug Deliv. Rev. 67 (2014) 55–68.

[8] A.E. Coron, J.S. Kjesbu, F. Kjærnsmo, J. Oberholzer, A.M.A. Rokstad, B.L. Strand, S. Modi, S.T. Rashid, B.L. Strand, Sulfated alginate pericapsular fibrotic overgrowth mitigated on encapsulated cGMPC-hPSC-hepaticocytes in mice, Front. Bioeng. Biotechnol. 9 (2022).

[9] J.M. Anderson, R. Rodriguez, D.T. Chang, Foreign body reaction to biomaterials, Semin. Immunol. 20 (2) (2008) 86–100.

[10] A.M.A. Roelapsed, I. Lacick, P. de Vos, B.L. Strand, Advances in biocompatibility and physico-chemical characterization of microspheres for cell encapsulation, Adv. Drug Deliv. Rev. 63 (2011) 111–130.

[11] O. Veiseh, J.C. Doloff, M.A. Roelapsed, H.H.T. Ham, C. Daub, L. Gazda, P. Thompson, L.R. Badell, A. Sambanis, C. Ricordi, C.J. Weber, Microencapsulated adult porcine islets transplanted intraperitoneally in streptozotocin-diabetic non-human primates, Transplantation 2025 (2018), e12450.

[12] V. Yamada, G. Fichman, J.P. Schneider, Serum protein adsorption modulates the inflammatory response induced by biomaterials in vivo, Faseb. J. 27 (7) (2013) 2768–2780.

[13] Z. Othman, B. Cillero Pastor, S. van Rijt, P. Habibovic, Understanding interactions between biomaterials and biological systems using proteomics, Biomaterials 29 (22) (2008) 3268–3277.

[14] P.R. Langer, D.G. Anderson, Combinatorial hydrogel library enables identification of materials that mitigate the foreign body response in primates, Nat. Biotechnol. 34 (3) (2016) 345–352.

[15] P. Soon-Shiong, R.E. Heintz, N. Merideth, Q.X. Yao, Z. Yao, T. Zheng, M. Murphy, A.E. Coron, J.S. Kjesbu, F. Kjærnsmo, J. Oberholzer, A.M.A. Rokstad, B.L. Strand, S. Modi, S.T. Rashid, B.L. Strand, Sulfated alginate pericapsular fibrotic overgrowth mitigated on encapsulated cGMPC-hPSC-hepaticocytes in mice, Front. Bioeng. Biotechnol. 9 (2022).

[16] J.M. Anderson, R. Rodriguez, D.T. Chang, Foreign body reaction to biomaterials, Semin. Immunol. 20 (2) (2008) 86–100.

[17] A.M.A. Roelapsed, I. Lacick, P. de Vos, B.L. Strand, Advances in biocompatibility and physico-chemical characterization of microspheres for cell encapsulation, Adv. Drug Deliv. Rev. 63 (2011) 111–130.

[18] J.M. Anderson, A. Rodriguez, D.T. Chang, Foreign body reaction to biomaterials, Drug Deliv. Rev. 67 (2014) 55–68.

[19] P. Soon-Shiong, R.E. Heintz, N. Merideth, Q.X. Yao, Z. Yao, T. Zheng, M. Murphy, A.E. Coron, J.S. Kjesbu, F. Kjærnsmo, J. Oberholzer, A.M.A. Rokstad, B.L. Strand, S. Modi, S.T. Rashid, B.L. Strand, Sulfated alginate pericapsular fibrotic overgrowth mitigated on encapsulated cGMPC-hPSC-hepaticocytes in mice, Front. Bioeng. Biotechnol. 9 (2022).

[20] J.M. Anderson, R. Rodriguez, D.T. Chang, Foreign body reaction to biomaterials, Semin. Immunol. 20 (2) (2008) 86–100.

[21] A.M.A. Roelapsed, I. Lacick, P. de Vos, B.L. Strand, Advances in biocompatibility and physico-chemical characterization of microspheres for cell encapsulation, Adv. Drug Deliv. Rev. 63 (2011) 111–130.

[22] O. Veiseh, J.C. Doloff, M.A. Roelapsed, H.H.T. Ham, C. Daub, L. Gazda, P. Thompson, L.R. Badell, A. Sambanis, C. Ricordi, C.J. Weber, Microencapsulated adult porcine islets transplanted intraperitoneally in streptozotocin-diabetic non-human primates, Transplantation 2025 (2018), e12450.

[23] A.J. Vegas, O. Veiseh, J.C. Doloff, M.A. Roelapsed, K.S. Hoem, A.E. Coron, G. Skjåk-Bræk, O.-L. Brekke, J. Hollister-Lock, T. Ekdahl, K.S. Hoem, A.E. Coron, G. Skjåk-Bræk, Heparin-Like properties of sulfated alginites with defined sequences and sulfation degrees, Biomacromolecules 15 (7) (2014) 2744–2750.
induced coagulation in human whole blood, Clin. Exp. Immunol. 182 (1) (2015) 81–89.

[44] T.E. Mollnes, O.-L. Brekke, M. Fung, H. Fure, D. Christiansen, G. Bergseth, V. Videm, K.T. Lappegård, J.K. Kold, J.D. Lambris, Essential role of the C5a receptor in E coli–induced oxidative burst and phagocytosis revealed by a novel lepratdin-based human whole blood model of inflammation, Blood 100 (5) (2002) 1869–1877.

[45] A. Hovland, R. Hardersen, E.W. Nielsen, T. Enebakk, D. Christiansen, K.T. Lappegård, G. Bergseth, J. Biomed. Mater. Res. 100A (5) (2012) 1142–1150.

[46] A. Sokolov, B.C. Hellerud, E.A. Johannessen, T.E. Mollnes, Inflammation response induced by candidate biomaterials of an implantable microfabricated sensor, J. Biomed. Mater. Res. 100A (5) (2012) 1142–1150.

[47] K. Oikonomopoulou, D. Ricklin, P.A. Ward, J.D. Lambris, Interactions between coagulation and complement–their role in inflammation, Semin. Immunopathol. 34 (1) (2012) 151–165.

[48] A.J. Gale, Continuing education course #2: current understanding of hemostasis, Toxicol. Pathol. 39 (1) (2011) 273–280.

[49] H. Weidmann, L. Heikaus, A.T. Long, C. Naundl, H. Schütler, T. Renne, The plasma contact system, a protease cascade at the nexus of inflammation, coagulation and immunity, Biochim. Biophys. Acta. Mol. Cell Res. 1864 (11 Pt B) (2017) 2118–2127.

[50] T.J. Girard, N.M. Lasky, E.A. Tuley, G.J. Broe Jr., Protein Z, protein Z-dependent protease inhibitor (serpinA10), and the acute-phase response, J. Thromb. Haemostas. JTH 11 (2) (2013) 375–378.

[51] P. Wojciechowski, J.L. Brash, The Vroman effect in tube geometry: the influence of flow on protein adsorption measurements, Journal of biomaterials science, Polym. Ed. 2 (3) (1991) 203–216.

[52] E.A. Vogler, Protein adsorption in three dimensions, Biomaterials 33 (5) (2012) 1201–1237.

[53] D.C. Briggs, A.W.W. Langford-Smith, H.H. Birchungs, T.A. Jowitt, C.M. Kelly, J.J. Engbli, C. Baldock, C.M. Milner, A.J. Day, Inter-a-inhibitor heavy chain-1 has an integron-like 3D structure mediating immune regulatory activities and matrix stabilization during ovulation, J. Biol. Chem. 295 (16) (2020) 17527–17540.

[54] B.T. Kim, H. Kitagawa, J. Tanaka, J. Tamura, K. Sugahara, In vitro heparan sulfate sequence of uronate residues in alginates, Carbohydr. Res. 68 (1) (1979) 23–28.

[55] E.A. Vogler, Protein adsorption in three dimensions, Biomaterials 33 (5) (2012) 1201–1237.

[56] J.A. Vizcaíno, A. Csordas, N. del-Toro, J.A. Dianes, J. Griss, I. Lavidas, G. Mayer, J. Biomed. Mater. Res. 100A (5) (2012) 2288–2296.

[57] J.A. Vizcaíno, A. Csordas, N. del-Toro, J.A. Dianes, J. Griss, I. Lavidas, G. Mayer, J. Biomed. Mater. Res. 100A (5) (2012) 2288–2296.

[58] M. Lekka, D. Saino-Seppe, A. Jakobsson, Hydrogel microspheres: Influence of chemical composition on the function of serum complement, Chemical engineering communications, 158 (2017) 158–168.

[59] H. Grasdalen, J.A. Vizcaíno, A. Csordas, N. del-Toro, J.A. Dianes, J. Griss, I. Lavidas, G. Mayer, J. Biomed. Mater. Res. 100A (5) (2012) 2288–2296.

[60] J.M. Schwenk, G.S. Omenn, Z. Sun, D.S. Campbell, M.S. Baker, C.M. Overall, Y. Benjamini, Y. Hochberg, Controlling the false discovery rate: a practical and powerful approach to multiple testing, J. Roy. Stat. Soc. B 57 (1) (1995) 289–300.

[61] D. Ricklin, G. Hajishengallis, K. Yang, J.D. Lambris, Complement: a key system for immune surveillance and homeostasis, Nat. Immunol. 11 (9) (2010) 785–797.

[62] G. Mayer, J. Biomed. Mater. Res. 100A (5) (2012) 2288–2296.

[63] B.T. Kim, H. Kitagawa, J. Tanaka, J. Tamura, K. Sugahara, In vitro heparan sulfate polymerization: crucial roles of core protein moieties of primer substrates in addition to the EXTL1-EXT2 interaction, J. Biol. Chem. 278 (43) (2003) 41618–41625.

[64] D. Ricklin, G. Hajishengallis, K. Yang, J.D. Lambris, Complement: a key system for immune surveillance and homeostasis, Nat. Immunol. 11 (9) (2010) 785–797.

[65] N.S. Merle, S.E. Church, V. Wasson-Bacchi, L.T. Roumenina, Complement system Part I – molecular mechanisms of activation and regulation, Front. Immunol. 6 (2015) 427–437.

[66] B.T. Kim, H. Kitagawa, J. Tanaka, J. Tamura, K. Sugahara, In vitro heparan sulfate polymerization: crucial roles of core protein moieties of primer substrates in addition to the EXTL1-EXT2 interaction, J. Biol. Chem. 278 (43) (2003) 41618–41625.

[67] D. Ricklin, G. Hajishengallis, K. Yang, J.D. Lambris, Complement: a key system for immune surveillance and homeostasis, Nat. Immunol. 11 (9) (2010) 785–797.

[68] B.T. Kim, H. Kitagawa, J. Tanaka, J. Tamura, K. Sugahara, In vitro heparan sulfate polymerization: crucial roles of core protein moieties of primer substrates in addition to the EXTL1-EXT2 interaction, J. Biol. Chem. 278 (43) (2003) 41618–41625.
[97] J.A. Voynow, M. Shinbashi, Neutrophil elastase and chronic lung disease, Biomolecules 11 (8) (2021) 1065.
[98] U. Valcourt, L.B. Akcaraz, J.Y. Exposito, C. Lethias, L. Bartholin, Tenascin-X, Beyond the architectural function, Cell Adhes. Migrat. 9 (1–2) (2015) 154–165.
[99] T. Liu, J.-M. Chen, D. Zhang, Q. Zhang, B. Peng, L. Xu, H. Tang, ApoPred: identification of apolipoproteins and their subfamilies with multifarious features, Front. Cell Dev. Biol. 8 (2021), 621144.

[100] H. Cui, D. Jiang, S. Banerjee, N. Xie, T. Kulkarni, R.M. Liu, S.R. Duncan, G. Liu, Monocyte-derived alveolar macrophage apolipoprotein E participates in pulmonary fibrosis resolution, JCI Insight 5 (5) (2020), e134539.
[101] T. Wang, S.S. Chen, R. Chen, D.M. Yu, P. Yu, Reduced beta 2 glycoprotein I improves diabetic nephropathy via inhibiting TGF-β/p38 MAPK pathway, Int. J. Clin. Exp. Pathol. 8 (3) (2015) 2321–2333.