INTRODUCTION
The advent of NiTi rotary instruments to the field of endodontics was a revolutionary change. These devices are made of pseudo-elastic alloy of nickel and titanium (Nitinol 55) and have an incredible influence on the mechanical preparations of root canals (1). The instrumentation of narrow and curved root canals can be challenging for many clinicians. Walia et al. showed that Nitinol files are at least two to three times more flexible than stainless steel (SS) files (2). The flexibility can enable the instrument to be used in curved and complex root canals with more facility and lower root canal shape alterations (3).

Many investigators have shown that the unexpected separation of NiTi rotary instruments, apart from higher strength and flexibility, remains a clinical challenge. This undesirable event can occur without any significant deformation seen on the surface of instrument (4). Different
causes, such as cyclic fatigue, static and dynamic torsional fatigue, have been attributed to the fracture of these devices (5). Cyclic fatigue is described by the alternating tension and compression cycles, which occur inside the structure of an instrument when it is moving through the maximum curvature of root canal (6). The cyclic fatigue is generally a concern in curved canals, and the many determinants such as radius and degree of canal curvature, instrument mass, diameter, taper, extended usage and also operator experience could contribute to the occurrence of this fatigue (5, 7-9). Torsional fatigue is considered to be another reason for instrument separation, which can also happen in straight root canals. This fatigue occurs due to instrument lock inside the canal, whereas the engine of hand piece is trying to rotate the shank of the instrument at the same time (7).

Investigations have been made to enhance the cyclic fatigue resistance of endodontic NiTi rotary instruments. Some authors have discussed whether new manufacturing methods can increase the fatigue resistance. Twisted method was introduced as one of the manufacturing methods that can increase the fatigue resistance of NiTi rotary instruments compared to the traditional grinding process (10). Other investigators reported that thermal treatments such as annealing of these instruments can enhance their fatigue resistance (11). Apart from reasons mentioned for the fatigue failure of NiTi instruments, others have suggested that the corrosion mechanisms, as a result of chemomechanical preparation and chemical disinfection or sterilisation, might be an initial factor for fatigue failure. These authors have questioned the effect of pitting or crevice corrosion on the surface of NiTi rotary instruments (12, 13).

Fretting corrosion occurs on the surface of corrosive substrate when it comes into contact with another surface during an oscillating movement. This issue was first seen for orthopaedic implants such as hip or knee joints, which resulted in corrosion of these implants and reduced the lifetime of these devices (14). There is a passivating oxide film of TiO2 on the surface of titanium and its alloys, which can be rubbed off or deteriorate due to low shear stresses such as rubbing toward another surface. Fretting corrosion is another reason for disruption of the passive oxide layer (14, 15). In the medical field, some authors have discussed fretting corrosion effect on crevice corrosion of modular hip tapers, which could accelerate the process of crevice corrosion (16). Based on the effect of pitting or crevice corrosion on cyclic fatigue failure of NiTi rotary instruments, it can be presumed that fretting corrosion is the initial process, which leads to crevice corrosion and finally resulting in cyclic fatigue failure (13).

There have been many types of solutions, which are used to prevent, inhibit and/or minimise corrosion. Corrosion inhibitors are one of the popular solutions that serve this goal (17-20). Generally, the corrosion inhibitors are categorised into two separate categories. First category includes the inhibitors that are coated on the surface of substrates in order to protect the substrate from any contact with oxidative agents, and the second category includes the migrating corrosion inhibitors (MCI), which should be applied when the substrate is under rehabilitation procedures. These inhibitors are able to penetrate into the substrate and remove the oxygen from the texture of substrate. This category of inhibitors contains basically mixtures of amines or alkoilichilic compounds (21, 22).

A novel anti-corrosive solution was recently patented (US patent 20160024311), which contains methoxy propyl amine (3-methoxypropyl-amine) (MOPA). MOPA is a colourless and clear liquid with ammoniacal odour, which is soluble in water and other organic solvents (23). MOPA has been used as a corrosion-inhibitory solution in steam condensate systems. The anti-corrosive effect of MOPA is due to its amine content (24). The present study aimed to evaluate the effect of different environments including deionised water, blood, PBS and MOPA on the cyclic fatigue resistance of endodontic NiTi rotary instruments. We determined whether MOPA can increase the fatigue resistance due to its anti-corrosive potential under in vitro conditions.

MATERIALS AND METHODS
A stainless-steel block, 110 mm wide (side-by-side), 100 mm long and 10 mm deep, was made of hardened stainless steel. This block was provided by using a Computer Numerical Control (CNC) device (Fig. 1a). The artificial canals were latched to the length of 16 mm, radius 5 mm and a 30-degree angle. Similar to a previously done study (25), an apparatus was used as a frame for supporting the rotary instrument hand piece for rotating the instruments inside the artificial canals.

Samples storage
Forty ProTaper F1 files (Maillefer-Dentsply, Baillagues, Switzerland) were selected and autoclaved two times and divided into four groups of 10 each (n=10). ProTaper F1 files were firstly rotated at 300 rpm for 30 s in the presence of PBS and then underwent two cycles of sterilisation at 121°C, 15 psi for 15 min. Thereafter, samples were immersed in 10-mL glass vials containing 5 mL of the following solutions for 24 h. G1: Deionised water (DW); G2: blood; G3: PBS and G4: novel anti-corrosive solution (MOPA) (pH=11.1). Blood was collected by a vein puncture needle 25×7 (Vacutainer) in a 5-mL tube with 5% anticoagulant EDTA, percentage by weight.

Cyclic fatigue testing
At first, all instruments were inserted into artificial canals to the full length and rotated using a 1:16 reduction Anthogyr hand piece (Sallanches, France) with a torque-controlled electric (speed=300 rpm, torque=70 Nm, according to manufacturer’s instructions). NCF has been recorded for each instrument (NCF=time×speed).

SEM analysis
Samples before and after sterilisation and also after file separation were evaluated by a scanning electron microscope. Machine was operating at 15 kV (Leo. 440i; Oxford Microscopy, Oxford, UK). Data were analysed by Kolmogorov–Smirnov test, Levene test, ANOVA test and Scheffe test using SPSS software version 21 (IBM Corp.; Armonk, NY, USA). The level of significance was set at P=0.05.
fatigue testing of NiTi endodontic rotary instruments reported that there are not any approved testing protocols introduced by the International Standard Organisation for this fatigue failure. They also concluded that nearly all studies of cyclic fatigue were performed in a glass or metal tube (28). In the present study, a stainless-steel block was selected, which after preparation of artificial canals, was subjected to experimental conditions.

The effect of different substances has been discussed on the behaviour of NiTi rotary devices (29). Alapati et al. (29) indicated that scanning electron microscopy observations of clinically failed instruments, suggestions are offered for improving their fracture resistance and can be used as method for fractography analysis. Previous authors have acclaimed that chemical material, such as irrigating solutions, disinfectants and sterilisation process, might have an adverse effect on the structure of NiTi instruments (12, 13). Peters et al. indicated that immersion in NaOCl at temperatures of 21°C and 60°C for 1 or 2 h can reduce cyclic fatigue resistance (30). Cheung et al. (31) investigated effect of different environments on low-cycle fatigue (LCF) of NiTi instruments. These authors addressed deionised water and sodium hypochlorite as corrosive substances, which can drastically influence the LCF behaviour of these instruments (31). The results of present study also

RESULTS
Mean±standard deviations of NCF for experimental groups were 1121884±289811 (DW), 845221±324871 (blood), 1432561±289851 (PBS) and 1978214±662101 (MOPA). Samples in blood and MOPA groups showed significantly lowest and highest NCF values, respectively (p<0.05). Samples in PBS samples showed significantly higher values than DW and blood samples (p<0.05) (Fig. 1b).

In the DW group, SEM results revealed impurities on the surface with irregular honeycomb pattern. In the blood group, images showed intergranular pattern with aggregation of chloride and nitrogen derived from blood on the fracture surface. In the PBS group, macro dimple pattern was observed, and in the MOPA group, a honeycomb pattern was observed with lower impurities (Fig. 2).

DISCUSSION
The separation of endodontic NiTi rotary instruments due to the cyclic or torsional fatigue is an obstacle in endodontic treatments. Although this does not occur all the time, but its occurrence leads to the failure of root canal therapies (26). Among all the reasons for cyclic fatigue failure, the radius of canal curvature is known to have the greatest role in this failure (27). Plotino et al. in their review of the literature on cyclic fatigue testing of NiTi endodontic rotary instruments reported that there are not any approved testing protocols introduced by the International Standard Organisation for this fatigue failure. They also concluded that nearly all studies of cyclic fatigue were performed in a glass or metal tube (28). In the present study, a stainless-steel block was selected, which after preparation of artificial canals, was subjected to experimental conditions.

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showed that deionised water can reduced the cyclic fatigue compared with PBS.

According to SEM images, chloride ion aggregation on the surface of samples stored in blood appears to be an important factor in decreasing of NCF. In a previous study, authors reported that NiTi-made alloys are primarily susceptible to corrosion when they come into contact with solutions that contain chlorides (32). Many authors have investigated the effect of chloride ion concentration on crevice corrosion of titanium (33). According to the fact that pitting or crevice corrosions can be regarded as an initiating factor for fatigue failure, it can be presumed that the conventional fatigue failure might be related to the corrosion fatigue. This issue can finally affect the instrument fatigue resistance (12, 13).

Fretting corrosion has been determined as a type of corrosion occurring as a result of oscillatory movements (14). During fretting corrosion, some fluctuations can be observed on the surface of titanium, which includes the removal of the passivating oxide layer (known as depassivation) and production of oxide layer (known as repassivation) at the corroded site that are in a dynamic equilibrium (34-36). One of the most basic limitations of the present study is its exclusive alteration of temperature of rotary systems during the application; therefore, we will aim to check this factor and the effect of failure in future studies. Results of NCF data in MOPA group showed an increase in cyclic fatigue resistance. This issue can be explained by the anti-corrosive behaviour of MOPA due to the effect of this substance on the oxide layer present on the surface of instrument. It appears that MOPA, by protecting the oxide layer from depassivation, can reduce the fluctuations mentioned above. This phenomenon can result in the reduction of fretting corrosion and finally affect the NiTi file corrosion fatigue resistance. The SEM images of this group also showed lesser impurities, which can be attributed to the protection of oxide layer from fretting and crevice corrosion.
CONCLUSION
1. Deionised water and chloride ions can be regarded as corrosive substances, which affect negatively on the lifetime of NiTi rotary instruments. This is mainly due to the crevice corrosion starting on the surface of instrument followed by fatigue failure and instrument separation. Thus, the use of NiTi rotary files in the bleeding root canals might be threatened in the presence of blood. However, the contact time in root canals is much lower than the storage time considered in this study.

2. The tested novel anti-corrosive solution (MOPA) could be suggested as an effective treatment with corrosion-inhibitory action. This substance can increase fatigue resistance and NCF of NiTi rotary files due to stabilisation of the passivating oxide layer. This can reduce the fretting corrosion process, which is considered as an acceleration for crevice corrosion.

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