Synthesis and evaluation of 2-chloro \(N\text{-}[(S)\text{-}[(S)\text{-}1\text{-}[^{11}\text{C}]\text{methylpiperidin-2-yl}]\text{(phenyl)methyl}]3\text{-}\text{trifluoromethyl-benzamide (}[^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)}\) as a PET radioligand for glycine transporter 1

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Abstract

Background: Dysfunction of the glycine transporter 1 (GlyT1) has been suggested to be involved in psychiatric disorders such as schizophrenia. GlyT1 inhibitors have therefore been considered to have antipsychotic therapeutic potential. Positron emission tomography (PET) imaging probes for GlyT1 are, consequently, expected to be useful for investigating the mechanism of such disease conditions and for measuring occupancy of GlyT1 inhibitors in vivo.

The aim of this study was to assess the potential of 2-chloro \(N\text{-}[(S)\text{-}[(S)\text{-}1\text{-}[^{11}\text{C}]\text{methylpiperidin-2-yl}]\text{(phenyl)methyl}]3\text{-}\text{trifluoromethyl-benzamide (}[^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)}\) as a PET imaging agent for GlyT1.

Methods: \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} was synthesized by \(N\text{-}[^{11}\text{C}]\text{methylation of SSR504734 via }[^{11}\text{C}]\text{CH}_3\text{OTf}\). In vitro brain distribution of \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} was tested in whole-hemisphere autoradiography (ARG) on human brain slices. Initial PET studies were performed using a cynomolgus monkey at baseline and after pretreatment with 0.1 to 1.5 mg/kg of SSR504734. Then, PET studies using rhesus monkeys were performed with arterial blood sampling at baseline and after pretreatment with 1.5 to 4.5 mg/kg SSR504734. Distribution volumes \(V_T\) were calculated with a two-tissue compartment model, and GlyT1 occupancy by SSR504734 was estimated using a Lassen plot approach.

Results: \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} was successfully synthesized in moderate radiochemical yield and high specific radioactivity. In the ARG experiments, \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} showed specific binding in the white matter and pons. In the initial PET experiments in a cynomolgus monkey, \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} showed high brain uptake and consistent distribution with previously reported GlyT1 expression in vivo (thalamus, brainstem > cerebellum > cortical regions). However, the brain uptake increased after pretreatment with SSR504734. Further PET studies in rhesus monkeys showed a similar increase of brain uptake after pretreatment with SSR504734. However, the \(V_T\) of \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} was found to decrease after pretreatment of SSR504734 in a dose-dependent manner. GlyT1 occupancy was calculated to be 45% and 73% at 1.5 and 4.5 mg/kg of SSR504734, respectively.

Conclusions: \([^{11}\text{C}]\text{N}\text{-}\text{methyl-SSR504734)} is demonstrated to be a promising PET radioligand for GlyT1 in nonhuman primates. The present results warrant further PET studies in human subjects.

Keywords: Glycine transporter 1, SSR504734, \(^{11}\text{C}\), Positron emission tomography, Schizophrenia

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**Background**

Glycine is a neurotransmitter of the inhibitory glycine receptors (GlyRs) but also serves as an essential co-agonist of the excitatory N-methyl-D-aspartate (NMDA) receptors [1,2]. It is known that the extracellular glycine concentration is modulated by two glycine transporters (GlyT1 and GlyT2) [3]. It has been suggested that GlyT2 is mainly implicated in the control of inhibitory neurotransmission via GlyRs, whereas GlyT1 is considered to regulate the glycine level in both inhibitory neuron and excitatory neurons [4-8].

It has been indicated that NMDA receptor dysfunction may be related to various disorders such as schizophrenia, Parkinson’s Disease, and Alzheimer’s Disease [9-11]. Schizophrenia has been hypothesized to be related to the hypofunction of NMDA receptors. Direct NMDA receptor agonists would cause severe side effects. Targeting the glycine site of the NMDA receptors has been suggested to be a promising therapeutic strategy through the facilitation of NMDA receptor functions [12-14]. Indeed, it was reported that enhancement of glycine concentration in the synaptic cleft by GlyT1 inhibitors, such as RG1678 (Figure 1), was efficacious in the treatment of the negative and cognitive symptoms of schizophrenia [11,15,16]. In addition, GlyT1 inhibitors could be potential therapeutic agents for various disorders associated with inhibitory neurotransmission (e.g., depression and neuropathic pain) [17,18].

Positron emission tomography (PET) is considered as one of the most useful imaging methods for noninvasive visualization of target proteins. Development of PET radioligands for GlyT1 is thus considered useful for obtaining information about various psychiatric diseases and occupancy of GlyT1 inhibitors in vivo. Several novel PET radioligands with high affinity to GlyT1 were reported recently. Among these radioligands, [11 C]GSK931145 and [18 F]MK-6577 (Figure 2) showed good brain uptake, good accumulation in GlyT1-rich regions, and significant blocking by GlyT1 ligands in the brain of pigs, rhesus monkeys, and humans [19-21].

The N-[Phenyl (piperidin-2-yl) methyl]benzamide derivative SSR504734 (Figure 1) is a selective and competitive inhibitor of GlyT-1 [22]. Since SSR504734 has moderate lipophilicity and a molecular weight of 397, SSR504734 may be a useful lead compound for the development of PET radioligands. Indeed, SSR504734-related radioligands such as [11 C]SA1 showed high brain uptake and a consistent accumulation with the GlyT1 distribution in the mouse and monkey brain [23]. More recently, we developed [125 I]-[S-(S)-1-methylpiperidin-2-yl] (phenyl)methyl]3-trifluoromethyl-benzamide ([125 I]IMPB) as a promising SPECT ligand candidate [24].

It was previously reported that N-methyl-SSR504734 has high affinity for GlyT1 (1.6 nM) [25] and a potent GlyT1 inhibitory activity (IC$_{50}$ = 2.4 nM) [24]. The same structure with [11 C]-N-methyl-SSR504734 was reported recently [23]. In vivo [11 C]N-methyl-SSR504734 showed high brain uptake; however, PET evaluation using non-human primates were not so far reported in the literature [23]. In this study, we aimed to synthesize [11 C]-N-methyl-SSR504734 and evaluate its distribution by in vitro autoradiography in human brain slices and by in vivo PET studies in monkeys.

**Methods**

**General**

SSR504734 and N-methyl-SSR504734 were synthesized according to the literature [25,26]. All other chemicals were obtained from commercial sources, were of analytical grade, and were used as received. Purification of [11 C]-N-methyl-SSR504734 was performed by a high-performance liquid chromatography (HPLC) system consisting of a Merck-Hitachi absorbance detector ($\lambda = 254$ nm; VWR International, Stockholm, Sweden) in series with a GM tube (Carroll-Ramsey, Berkely, CA) for radioactivity detection. The purified [11 C]-N-methyl-SSR504734 was analyzed by a HPLC system consisting of a Merck-Hitachi L-7100 Pump, L-7400 UV detector, and GM tube for radioactivity detection (VWR international). The radiometabolism of each product in monkey plasma was assessed with HPLC on a system that contained a Merck-Hitachi D-7000 interface module, L-7100 pump and an L-7400 absorbance detector ($\lambda = 254$ nm; Merck-Hitachi, Tokyo, Japan), and an

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**Figure 1** Chemical structure of GlyT1 inhibitors.
injector (7125 with a 5.0-ml loop; Rheodyne, Cotati, CA, USA) equipped with a μ-Bondapack-C18 column (300 × 7.8 mm, 10 μm; Waters, Milford, MA, USA) in series with a 150TR radiodetector (Packard Radiomatic, PerkinElmer, Waltham, MA, USA) equipped with a PET flow cell (550 μl).

Preparation of \([^{11}C]\)N-methyl-SSR504734

Ultrahigh specific activity of \([^{11}C]\)CH3I and \([^{11}C]\)CH3OTf was prepared from \([^{11}C]\)CH4 as described previously [27]. In brief, \([^{11}C]\)CH4 was obtained via \(^{14}\)N(p,α)\(^{11}\)C reaction on nitrogen containing 10% hydrogen with 16 MeV protons. \([^{11}C]\)CH4 reacted with iodine at high temperature in a heated quartz column and converted to \([^{11}C]\)CH3I. \([^{11}C]\)CH3OTf was prepared by carrying \([^{11}C]\)CH3I vapor through a heated glass column containing silver triflate-impregnated graphitized carbon. The \([^{11}C]\)CH3I or \([^{12}C]\)CH3OTf was trapped in a vessel containing SSR504734 (0.6 mg, 1.51 μmol), organic solvent (DME, acetone or CH3CN; 400 μl), and base (NaH or NaOH; 5 μmol). After 3 min, the radioactive reaction mixture was purified by an HPLC (column, ACE5 C18-HL, 250 × 10 mm; mobile phase, CH3CN: 0.1 M NH4HCO3 in H2O = 45:55; flow rate, 6.0 ml/min). The solvents in the collected product fraction were evaporated at 70°C, and the final product was formulated in phosphate buffered saline (PBS; pH = 7.4). The purity of the product was analyzed by an HPLC (column, μ-Bondapak C18 10 μm 125 Å 7.8 × 300 mm; mobile phase, CH3CN: 0.1% TFA in H2O = 30:70; flow rate, 2.0 ml/min) and identified by co-injection of reference N-methyl-SSR504734.

In vitro autoradiography

Human brains without pathology were obtained from the National Institute of Forensic Medicine, Karolinska Institutet (Stockholm, Sweden) as well as from the Department of Forensic and Insurance Medicine, Semmelweis University, Budapest. After the removal of the brains (6- and 11-h post mortem times), they were kept at −85°C until sectioning; after which, the whole hemisphere brain slices were kept at −25°C until the autoradiographic procedures. Ethical permissions were obtained from the relevant research ethics committee of the respective institutions. The sectioning of the brains and the autoradiography experiments were performed at the Department of Clinical Neuroscience, Karolinska Institutet. The cryosectioning took place on a Leica cryomacrocut system (San Marcos, CA, USA) [28,29]. Horizontal sections (100 μm thick, containing cerebral cortex, white matter, cerebellum, and pons) and coronal sections (100 μm thick, containing cerebral cortex, white matter, putamen, and caudate nucleus) were used. The sections were incubated in binding buffer (120 mM NaCl, 2 mM KCl, 1 mM MgCl2, 1 mM CaCl2, and 50 mM Tris–HCl, pH 7.5) containing \([^{11}C]\)N-methyl-SSR504734 (40 MBq) at 25 °C for 30 min. To determine the nonspecific binding, unlabelled N-methyl-SSR504734 (10 μM) was included in
the incubation buffer for anatomically adjacent sections. For comparison with other GlyT1 radioligands, blocking was also made with SSR504734 (10 μM). The slices were rinsed thrice for 3 min each with cold (5°C) washing buffer (120 mM NaCl, 50 mM Tris-HCl, pH = 7.5) and subsequently dipped into cold water. The slides were then placed on an imaging plate (Fujiﬁlm Plate BAS-TR2025, Fujiﬁlm, Tokyo, Japan) for 20 min. The plates were developed, and the resulting images were processed in a Fujiﬁlm BAS-5000 phosphorimager (Fujiﬁlm, Tokyo, Japan). Aliquots (20 μl) of the incubation solution were spotted onto polyethylene-backed absorbent paper (Bench-Guard™, Lennox, Dublin, Ireland), allowed to dry, scanned, and digitized in the phosphorimager parallel with the tissue scans. The autoradiography (ARG) signal’s optical density was measured using Multi Gauge 3.2 image analysis software (Fujiﬁlm, Tokyo, Japan).

PET studies in monkeys

PET measurements were performed using a high-resolution research tomograph (CTI/Siemens Molecular Imaging, Knoxville, TN, USA) with an in-plane resolution less than 1.5 mm FWHM in the center of the FOV [30]. PET data were acquired by list mode. The data were reconstructed with a series of frames (5 × 1 min, 5 × 3 min, 5 × 6 min, and 13 × 10 min) using the Ordinary Poisson-3D-Ordered Subset Expectation Maximization (OP03D-OSEM) algorithm with 10 iterations and 16 subsets including modeling of the points spread function. Image reconstruction was performed on a quad-core PC running a fast reconstruction algorithm [31].

One female cynomolgus monkey (4,900 and 5,200 g at different PET days) and two female rhesus monkeys (5,550 and 5,550 g) were used in this study. The study was approved by the Animal Ethics Committee of the Swedish Animal Welfare Agency (Dnr 145/08 and 386/09) and was performed according to the ‘Guidelines for Planning, Conducting and Documenting Experimental Research’ (Dnr 4820/06-600) of the Karolinska Institutet as well as the ‘1996 Guide for the Care and Use of Laboratory Animals’.

Anesthesia was induced by intramuscular injection of ketamine hydrochloride (60 mg) and maintained by the administration of a mixture of sevoflurane, O2, and medical air after endotracheal intubation. The head was immobilized with a fixation device. Body temperature was maintained by Bair Hugger Model 505 (Ariszant Healthcare, MN, USA) and monitored by an esophageal thermometer. ECG, heart rate, respiratory rate, and oxygen saturation were continuously monitored throughout the experiments. Blood pressure was monitored every 5 min.

Magnetic resonance images (MRIs) of each monkey brain were previously obtained using a 1.5 T General Electrics Signa system (GE, Milwaukee, WI, USA). PET measurements consisted of two parts, as follows.

PET measurements using a cynomolgus monkey

PET measurements were performed for 123 min immediately after intravenous (i.v.) injection of radioligand at baseline and after pretreatment with SSR504734. SSR504734 was administered over 15 min, starting 30 min before the radioligand injection. PET measurements were performed on two separate days at a 6-week interval. One baseline PET measurement and one PET measurement after pretreatment with 0.1 mg/kg of SSR504734 were performed on the first day. One baseline PET measurement and two PET measurements after pretreatment with 0.5 and 1.5 mg/kg of SSR504734 were performed on the second day.

During each PET measurement, venous blood samples were taken from a femoral vein for the measurement of [11 C] N-methyl-SSR504734 protein binding at 5 min before the radioligand injection and for metabolite analysis of [11 C]N-methyl-SSR504734 at 4,15, 30, 60, 90, and 120 min after the radioligand injection.

PET measurements using rhesus monkeys

PET measurements were performed for 123 min immediately after i.v. injection of radioligand at baseline and after pretreatment with SSR504734. SSR504734 was administered over 15 min, starting 30 min before the radioligand injection. PET measurements were performed on two separate days with two monkeys. One baseline PET measurement and one PET measurement after pretreatment with 1.5 mg/kg of SSR504734 were performed on one monkey. One baseline PET measurement and one PET measurement after pretreatment with 4.5 mg/kg were performed on the other monkey.

During each PET measurement, arterial blood was collected continuously for 3 min using an automated blood-sampling system at a speed of 3.0 mL/min (Allog AB, Molndal, Sweden). Blood samples (1.0 to 2.5 mL) were drawn at 4, 15, 30, 60, 90, and 120 min after the radioligand injection for blood and plasma radioactivity and metabolite correction. One arterial blood sample (2.0 ml) was taken 5 min before the radioligand injection for the measurement of [11 C]N-methyl-SSR504734 protein binding.

Metabolite analysis

From the obtained blood samples, plasma was obtained after centrifugation at 2,000 × g for 2 to 4 min and was mixed with 1.4 times the volume of acetonitrile. The supernatant acetonitrile-plasma mixture obtained after centrifugation at 2,000 × g for 2 to
4 min was injected into the radio-HPLC system. HPLC analysis was performed on a Waters \( \mu \)-Bondapak-C\(_{18} \) column (300 × 7.8 mm, 10 \( \mu \)m) by gradient elution using (a) ammonium formate (100 mM) and (b) acetonitrile at 6.0 mL/min.

Measurement of protein binding

Monkey plasma (500 \( \mu \)L), or PBS (500 \( \mu \)L) as a control, was mixed with \([^{11}C]\)N-methyl-SSR504734 solution (50 \( \mu \)L, approximately 1 MBq) and incubated at room temperature for 10 min. Samples (20 \( \mu \)L) from each incubation mixture were measured with a well counter. After the incubation, 200-\( \mu \)L portions of the incubation mixtures were pipetted into ultrafiltration tubes (Millipore Centrifree YM-30, Merck Millipore, Billerica, MA, USA) and centrifuged for 15 min at 1,500 \( \times \) g. Samples (20 \( \mu \)L) from each filtrate were pipetted for counting. The results were corrected for the membrane binding as measured with the control samples.

Data analysis

Regions of interest (ROI) for the thalamus, cerebellum, caudate, putamen, frontal cortex, temporal cortex, anterior cingulate cortex, pons, white matter, and the whole-brain contour were delineated on PET/MRI co-registered brain images for each monkey. Co-registrations and ROI delineations were performed using PMOD 3.0 (Pixel-Wise Modeling Computer Software, PMOD Group, Zurich, Switzerland). PET data were analyzed using several parameters such as percent injected dose (%ID) and percent standard uptake value (%SUV), where

\[
%ID = \frac{\text{total radioactivity in the whole brain (MBq)}}{\text{injected radioactivity (MBq)}} \times 100
\]

\[
%SUV = \frac{\text{radioactivity (MBq/cc)}}{\text{injected radioactivity (MBq)}} \times \frac{\text{body weight (g)}}{100}
\]

In the PET measurements using rhesus monkeys, the total distribution volume (\( V_T \)) was calculated by a two-tissue compartment model as well. GlyT1 occupancy was estimated by applying Lassen plot approach [32], which can determine nondisplaceable distribution volume (\( V_{ND} \)) and occupancy using \( V_T \) values at baseline and after pretreatment. Seven regions (the pons, cerebellum, putamen, frontal cortex, caudate, anterior cingulate cortex, and temporal cortex) were used for the plot.

Results

Radiochemistry

When \([^{11}C]\)CH\(_3\)I was applied as a methylating agent and NaH or NaOH as a base, the desired \([^{11}C]\)N-methyl-SSR504734 was not obtained in significant yield. On the other hand, in the case where \([^{11}C]\)CH\(_3\)OTf was used in the reaction instead of \([^{11}C]\)CH\(_3\)I, \([^{11}C]\)N-methyl-SSR504734 was successfully synthesized. The highest radiochemical yield (36% to approximately 42%) was achieved by using NaOH as a base and CH\(_3\)CN as a solvent (Table 1 and Scheme 1). Specific activity of the ligand was calculated.
to be 1,420 to 1,860 GBq/μmol \((N = 3)\) at the time when the synthesis of \([^{11}C]N\)-methyl-SSR504734 was completed. The ultrahigh specific activity of the radioligand was consistent with our previous results by using \([^{11}C]\) CH₄ as a starting precursor [27].

**In vitro ARG of human brain slices**

In the postmortem autoradiography study *in vitro*, \([^{11}C]\) N-methyl-SSR504734 showed a rather homogenous accumulation in the human brain slices including the temporal cortex, white matter, caudate nucleus, putamen,

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**Figure 3** *In vitro* postmortem autoradiography study of human brain. Autoradiogram from coronal (panels A, B, and C; 100-mm thickness) and horizontal whole-hemisphere (panels D, E, and F; 100-mm thickness) cryosections of the human brain incubated with \([^{11}C]N\)-methyl-SSR504734 under baseline (panels A and D), blocked by non-radioactive \(N\)-methyl-SSR504734 (10 \(\mu\)M; panels B and E), and blocked by SSR504734 (10 \(\mu\)M; panels C and F) conditions. The quantified values of \([^{11}C]N\)-methyl-SSR504734 (C) were expressed as (PSL-BG)/mm² (panel G). TC, temporal cortex; PUT, putamen; CAU, caudate nucleus; CB, cerebellum; WM, white matter.
pons, and cerebellum (Figure 3A,D). The reduction of \([^{11}\text{C}]N\)-methyl-SSR504734 binding by non-radioactive \(N\)-methyl-SSR504734 and SSR504734 was prominent in the white matter and pons, but in other regions, the degree of the reduction was small (Figure 3).

**PET measurements using a cynomolgus monkey**

The injected radioactivity was 144.4 ± 16.5 MBq. Specific radioactivity was higher than 234 GBq/μmol at the time of injection. The corresponding injected mass was less than 0.3 μg.

The summation images are shown in Figure 4. In the baseline PET measurements (\(N = 2\)), time-activity curves (TACs) of \([^{11}\text{C}]N\)-methyl-SSR504734 in whole brain reached peak (2.8%ID to 3.1%ID) at 24 min, followed by a moderate decline (Figure 5A). The rank order of regional brain uptake was as follows: thalamus > pons > cerebellum ≈ putamen > cortical regions > white matter (Figures 4A and 5B), which was basically consistent with \textit{in vivo} regional brain uptake with other PET radioligands [19-21]. The radioactivity level of \([^{11}\text{C}]N\)-methyl-SSR504734 was increased in all regions after pretreatment with SSR504734 in a dose-dependent manner (Figures 4B,C and 5C,D).

The parent fraction of \([^{11}\text{C}]N\)-methyl-SSR504734 in the plasma was reduced during PET measurements. The metabolite rate was similar during baseline and pretreatment conditions with SSR504734 (Figure 6A). Radiochromatograms showed that more hydrophilic metabolites of \([^{11}\text{C}]N\)-methyl-SSR504734 only were detected in the plasma (Figure 6B,C). Protein binding of \([^{11}\text{C}]N\)-methyl-SSR504734 was 87% to 91% at baseline and after pretreatment.

**PET measurements using rhesus monkeys**

The injected radioactivity was 170.0 ± 2.4 MBq. Specific radioactivity was higher than 353 GBq/μmol at the time of injection. The injected mass was less than 0.2 μg.

In the baseline PET measurements (\(N = 2\)), TACs of \([^{11}\text{C}]N\)-methyl-SSR504734 in the whole brain reached peak (3.2%ID, 172%SUV to 188%SUV) at 16.5 to 42 min. The rank order of regional brain uptake was as follows: thalamus > pons > putamen > frontal cortex = temporal cortex > cerebellum > > white matter, as shown in Figures 7A and 8A. The brain distribution of \([^{11}\text{C}]N\)-methyl-SSR504734 was similar to that of the cynomolgus monkey. Likewise, pretreatment with SSR504734 (1.5 and 4.5 mg/kg) caused increase of \([^{11}\text{C}]N\)-methyl-SSR504734 binding in the brain.
SSR504734 uptake in the brain regions (Figures 7B and 8B) and considerable rise of the AUC of the arterial input function both at early and late phases (Figure 8C) in the PET studies of rhesus monkey 2. $V_T$ values in the brain regions of the rhesus monkeys analyzed by 2TC were shown in Table 2. $V_T$ could not be obtained robustly for the white matter. In the baseline PET measurement of rhesus monkey 1, $V_T$ in GlyT1-rich regions such as the thalamus and pons were at a high level (31.0 to 35.2), whereas comparable $V_T$ values were observed in other regions (23.1 to 28.6). After pretreatment of SSR504734 (1.5 and 4.5 mg/kg), $V_T$ decreased approximately 20% and 33% reduction of $V_T$ values in the whole brain as shown in Table 2.

Using Lassen plot, a linear fitting to the data points from seven brain regions was obtained for the dose of 1.5 and 4.5 mg/kg of SSR504734 (Figure 9A, B). Target occupancy was calculated to be 45.2% and 74.3% at 1.5 and 4.5 mg of SSR504734, respectively (Figure 9C).

The estimated $V_{ND}$ values from the graphical analysis in Figure 9A, B were 16.5 and 7.5, respectively. Percentage of $V_{ND}$ in $V_T$ was 52% to 66% and 39% to 56% at 1.5- and 4.5-mg doses of SSR504734, respectively (Table 3).

**Discussion**

In the present study, $[^{11}C]$N-methyl-SSR504734 was demonstrated to be a promising PET radioligand to measure GlyT1 occupancy in nonhuman primates. $[^{11}C]$N-methyl-SSR504734 was synthesized successfully using $[^{11}C]$CH$_3$OTf with moderate radiochemical yield and ultrahigh specific radioactivity compared with previously reported GlyT1 imaging [19,20,23].

In the *in vitro* ARG studies of human brain slices, $[^{11}C]$N-methyl-SSR504734 showed specific binding in
Figure 6 Fraction of $\left[{^1^1}C\right]$N-methyl-SSR504734 in the plasma during PET measurements. Percentage of unmetabolized $\left[{^1^1}C\right]$N-methyl-SSR504734 in the plasma of a cynomolgus monkey at baseline and pretreatment conditions (0.5 or 1.5 mg/kg of SSR504734) (A). HPLC analysis of plasma samples at 4 (C) and 90 min (D) after injection of $\left[{^1^1}C\right]$N-methyl-SSR504734 at baseline.

Figure 7 PET images of rhesus monkey 2. PET images in the transaxial (left), the sagittal (middle), and the coronal (right) slices of rhesus monkey 2 acquired from 9 to 123 min after intravenous injection with $\left[{^1^1}C\right]$N-methyl-SSR504734 at the baseline (A) and 4.5 mg/kg of pretreatment (B) conditions, and the corresponding MRI-T1 image (C).
GlyT1-rich regions such as the white matter and pons. However, as only small decrease of $[^{11}C]N$-methyl-
SSR504734 binding was detected, nonspecific binding
was expected to be high in all brain regions (Figure 3).
Previously, $[^{125}I]$IMPB, which is a $[^{11}C]N$-methyl-
SSR504734 analog, showed excellent high specific bind-
ing to rat brain slices under *in vitro* ARG studies. In
addition, both IMPB and $N$-methyl-SSR504734 showed
very high inhibitory activity against the human GlyT1
(IMPB, $IC_{50} = 2.4$ nM; $N$-methyl-SSR504734, $IC_{50} = 7.5$
nM) as determined in a $[^3H]$glycine uptake assay using
JAR cells [24]. Therefore, it was suggested that this series
of compounds can bind to both rodent and human GlyT1. The present human ARG results seemed not to
be in line with the previous report [24]. Several factors
such as species differences and condition of the ARG
slices should be taken into consideration.

In PET studies using cynomolgus and rhesus monkeys,
$[^{11}C]N$-methyl-SSR504734 showed high brain uptake
and a regional brain distribution consistent with other
GlyT1 PET ligands [19-21]. The low $^{11}$C radioactivity in
the white matter, where GlyT1 binding was reported to
Figure 8 Time-activity curves of brain radioactivity after intravenous injection of $[^{11}C]N$-methyl-SSR504734 in rhesus monkey 2. (A) %
SUV in brain regions at baseline condition. (B) %SUV in brain regions at pretreatment conditions (4.5 mg/kg of SSR5047). Black square, thalamus;
white circle, pons; black triangle, cerebellum; white diamond, putamen; asterisk, frontal cortex; cross, white matter; black circle, caudate; white
square, anterior cingulate cortex; white triangle, temporal cortex. (C) Time-activity curve (%SUV) of metabolite-corrected radioactivity in the plasma
under baseline condition and pretreatment (4.5 mg/kg of SSR50474) condition.

Table 2 Total distribution volume ($V_t$) in brain regions of the rhesus monkeys analyzed by 2TC model

| Animal          | Parameter     | THA | Pons | CB | CAU | PUT | FC | ACC | TC | WB |
|-----------------|---------------|-----|------|----|-----|-----|----|-----|----|----|
| Rhesus monkey 1 | $V_t$ (baseline) | 31.0| 35.2 | 23.7| 26.2| 26.7| 25.2| 28.6| 25.6| 23.1|
|                 | $V_t$ (Blocking (1.5 mg/kg)) | 29.6| 26.8 | 20.4| 22.0| 22.8| 20.6| 22.5| 21.8| 18.6|
|                 | % decrease of $V_t$ | 4.5 | 23.9 | 13.9| 16.0| 14.6| 18.3| 21.3| 14.8| 19.5|
| Rhesus monkey 2 | $V_t$ (baseline) | 15.7| 16.9 | 12.8| 17.0| 15.8| 14.3| 15.5| 12.3| 12.6|
|                 | $V_t$ (Blocking (4.5 mg/kg)) | 11.9| 10.9 | 9.0 | 9.2 | 10.1| 8.6 | 9.0 | 8.9 | 8.5 |
|                 | % decrease of $V_t$ | 24.2| 35.5 | 29.7| 45.9| 36.1| 39.9| 41.9| 27.6| 32.5|

*Percent decrease of values from baseline study to blocking study. ACC, anterior cingulate cortex; CAU, caudate; CB, cerebellum; FC, frontal cortex; PUT, putamen;
TC, temporal cortex; THA, thalamus; WB, whole brain.
be high in *in vitro* ARG studies, was consistent with our previous *ex vivo* studies of $[^{125}\text{I}]$IMPB [24] and previous PET studies with other GlyT1 ligands [19-21]. Compared with *in vitro* ARG results, low uptake in the white matter might be related to low blood flow in the white matter [33,34].

$V_T$ values of white matter could not be obtained reliably with the 2TC model. Although several other quantitative methods such as Logan plot were investigated, they did not work well (data not shown). This unreliable estimation of $V_T$ might be related in part to time-activity curves in the white matter being relatively noisy due to

Table 3 Percentage of $V_{ND}$ in total distribution volume in rhesus monkeys

| Study                        | Parameter | Pons | CB | CAU | PUT | FC | ACC | TC |
|------------------------------|-----------|------|----|-----|-----|----|-----|----|
| Baseline + blocking (1.5 mg/kg) | $V_T$ | 31   | 35.2 | 23.7 | 26.2 | 26.7 | 25.2 | 28.6 |
|                              | $V_{ND}$ | 16.5 | 16.5 | 16.5 | 16.5 | 16.5 | 16.5 | 16.5 |
|                              | % of $V_{ND}$ in $V_T$ | 66   | 50  | 55  | 55  | 52  | 59  | 54  |
| Baseline + blocking (4.5 mg/kg) | $V_T$ | 16.9 | 12.8 | 17  | 15.8 | 14.3 | 15.5 | 12.3 |
|                              | $V_{ND}$ | 7.5  | 7.5  | 7.5  | 7.5  | 7.5  | 7.5  | 7.5  |
|                              | % of $V_{ND}$ in $V_T$ | 56   | 42  | 56  | 53  | 48  | 52  | 39  |

ACC, anterior cingulate cortex; CAU, caudate; CB, cerebellum; FC, frontal cortex; PUT, putamen; TC, temporal cortex; $V_{ND}$, nondisplaceable distribution; $V_T$, volume distribution volume.
potential spillover from the cortex and, in part, to \([^{11} \text{C}]\)N-methyl-SSR504734 kinetics being slower in the white matter than in other brain regions.

Although over 70\% of \([^{11} \text{C}]\)N-methyl-SSR504734 was metabolized within 90 min after injection of \([^{11} \text{C}]\)N-methyl-SSR504734, only higher hydrophilic fraction was observed (Figure 6B,C). Because these metabolites of \([^{11} \text{C}]\)N-methyl-SSR504734 are unlikely to penetrate the blood brain barrier, they are expected to have little influence on the in vivo brain distribution pattern of \([^{11} \text{C}]\)N-methyl-SSR504734.

The radioactivity concentration in the brain increased after pretreatment with SSR504734 in both the cynomolgus and rhesus monkeys. \([^{11} \text{C}]\)SA1, which is a structurally analogous compound of \([^{11} \text{C}]\)N-methyl-SSR504734, has been reported to show similar increase in brain uptake after pretreatment with SSR504734 in rhesus monkeys [23]. \([^{11} \text{C}]\)SA1 did not show the conclusive decrease of \(V_T\) due to large variability of \(V_T\). On the other hand, distribution volumes of \([^{11} \text{C}]\)N-methyl-SSR504734 were found to decrease after pretreatment with SSR504734 in a dose-dependent manner. In the monkeys, \([^{11} \text{C}]\)N-methyl-SSR504734 showed faster receptor kinetics than \([^{11} \text{C}]\)SA1, thereby providing the equilibrium between brain and plasma, and allowing more reliable estimation of \(V_T\) values.

In the Lassen plot analysis, seven regions were used for occupancy calculation. The thalamus seemed to behave differently from other regions in the plot, indicating that the thalamus might have a different nondisplaceable distribution volume or a different GlyT1 occupancy.

The estimated target occupancy by SSR504734 was increased dose-dependently (Figure 9), indicating that \([^{11} \text{C}]\)N-methyl-SSR504734 could be a promising PET ligand for occupancy studies of GlyT1 blockers. \([^{11} \text{C}]\)GSK931145 demonstrated good brain penetration and usefulness for GlyT1 occupancy study in monkeys [21]. However, poor test-retest results were reported in human subjects. It might be related to a little difference in the brain kinetics of \([^{11} \text{C}]\)GSK931145 between monkey and human subjects. It would be important to investigate whether there is species difference in the brain kinetics of \([^{11} \text{C}]\)N-methyl-SSR504734 between monkey and human subjects.

The present monkey PET study was performed under anesthesia induced by ketamine and maintained by sevoflurane. As ketamine is known to block NMDA receptors as an open channel blocker, and sevoflurane is a noncompetitive antagonist of NMDA receptor, an indirect interaction between these two anesthesia drugs and glycine transporter 1 function via NMDA receptors cannot be excluded. The use of anesthetics should be taken into account when the radioligand is considered for further evaluation.

In the present study, SSR504734 was used as a blocker. As SSR504734 is a structurally analogous compound to \([^{11} \text{C}]\)N-methyl-SSR504734, the possibility of interaction at a nonspecific binding site was not completely excluded. If the blocking occurs at a nonspecific binding site, estimated \(V_{ND}\) by Lassen plot would be close to zero. Considering the estimated \(V_{ND}\) by Lassen plot shown in Figure 9, the possibility were considered to be low. To exclude the possibility completely, blocking study by compounds with different chemical structure should be performed in future study.

Conclusions

In this study, \([^{11} \text{C}]\)N-methyl-SSR504734 was successfully synthesized and evaluated as a candidate PET radioligand for GlyT1. \([^{11} \text{C}]\)N-methyl-SSR504734 showed a regional accumulation, which was consistent with previous reports on the GlyT1 distribution. \(V_T\) values were decreased by SSR504734 in a dose-dependent manner, suggesting specific binding. Considering these results, \([^{11} \text{C}]\)N-methyl-SSR504734 is a promising PET radioligand for GlyT1. The present study warrants further PET studies in human subjects.

Competing interests

The authors declare that they have no competing interests.

Authors’ contributions

TF, AT, and CH carried out the design of this study and drafted the manuscript. TF, YM, MH, and MN participated in the syntheses of SSR504734 and N-methyl-SSR504734. TF, ZJ, and JDA carried out the radiosynthesis of \([^{11} \text{C}]\)N-methyl-SSR504734. TF and BS carried out the autoradiography studies. AT, BG, SF, and JDA participated in the PET studies. RN carried out the metabolite analysis and measurement of protein binding. AT and CH participated in the data analysis, data interpretation, and revising of the manuscript. All authors read and approved the final manuscript.

Acknowledgments

The authors thank the members of the Karolinska Institutet PET Center for their assistance in the PET experiments. We also thank Siv Eriksson for the excellent technical assistance with the autoradiography experiments and Gudrun Nylen for the excellent technical assistance in the PET studies. Financial support for this study was provided by the grant from the Ichiro Kanehara Foundation and the grant ‘Institutional Program for Young Researcher Overseas Visits’ from the Japan Society for the Promotion of Science (JSPS).

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Received: 2 April 2012 Accepted: 1 June 2012
Published: 9 July 2012

References

1. Danytisz W, Parsons CG: Glycine and N-methyl-D-aspartate receptors: physiological significance and possible therapeutic applications. Pharmacol Rev 1998, 50:597–564.
2. Legendre P: The glycineric inhibitory synapse. Cell Mol Life Sci 2001, 58:760–793.
3. Eulenburg V, Arnsen W, Betz H, Gomeza J: Glycine transporters: essential regulators of neurotransmission. Trends Biochem Sci 2000, 30:325–333.
4. Zafra F, Aragon C, Olivares L, Danbolt NC, Gimenez C, Storn-Mathisen J: Glycine transporters are differentially expressed among CNS cells. J. Neurosci 1995, 15:3952–3969.

5. Jurkowska R, Nelson N: Localization of glycine neurotransmitter transporter (GLYT2) reveals correlation with the distribution of glycine receptor. J. Neurochem 1995, 64:1026–1033.

6. Roux MJ, Supplisson S: Neuronal and glial glycine transporters have different stoichiometries. Neuroreport 2000, 11:25–33.

7. Gomez A, Hu Ismann S, Ohno K, Eulenburg V, Szo Ke K, Richter D, Betz H: Inactivation of the glycine transporter 1 gene discloses vital role of glial glycine uptake in glycine inhibition. Neuroreport 2003, 40:785–796.

8. Cubelos B, Gme Nez C, Zafra F: Localization of the GLYT1 glycine transporter at glutamatergic synapses in the rat brain. Cereb Cortex 2005, 15:446–459.

9. Kemp JA, McKean RM: NMDA receptor pathways as drug targets. Nat Neurosci 2002, 5(Suppl):1039–1042.

10. Javitt DC: Glutamate as a therapeutic target in psychiatric disorders. Mol Psychiatry 2004, 9:984–979.

11. Javitt DC: Glycine transport inhibitors for the treatment of schizophrenia: symptom and disease modification. Curr Opin Drug Discov Dev 2009, 12:468–478.

12. Kalia LV, Kalia SK, Salter MW: NMDA receptors in clinical neurology: excitatory times ahead. Lancet Neurol 2008, 7:472–755.

13. Yang CR, Svensson KA: Allosteric modulation of NMDA receptor via glycine uptake in glycinergic inhibition. Neuroreport 2003, 40:785–796.

14. Labrie V, Roder JC: The involvement of the NMDA receptor D-serine in the pathophysiology and treatment of schizophrenia. Neurosci Biobehav Rev 2009, 33:351–372.

15. Wolkenberg SE, Sur C: Recent progress in the discovery of non-sarcosine based GlyT1 inhibitors. Curr Top Med Chem 2010, 10:170–186.

16. Hashimoto K: Glycine transporter-1: a new potential therapeutic target for schizophrenia. Curr Pharm Des 2011, 17:112–120.

17. Dohi T, Morita K, Kitayama T, Motoyama N, Morioka N: Glycine transporter at glutamatergic synapses in the rat brain. Cereb Cortex 2005, 15:232–332.

18. Labrie V, Roder JC: The involvement of the NMDA receptor D-serine /glycine site in the pathophysiology and treatment of schizophrenia. Neurosci Behav Rev 2010, 34:351–372.

19. Wolkenberg SE, Sur C: Recent progress in the discovery of non-sarcosine based GlyT1 inhibitors. Curr Top Med Chem 2010, 10:170–186.

20. Hashimoto K: Glycine transporter-1: a new potential therapeutic target for schizophrenia. Curr Pharm Des 2011, 17:112–120.

21. Dohi T, Morita K, Kitayama T, Motoyama N, Morioka N: Glycine transporter inhibitors as a novel drug discovery strategy for neuropathic pain. Pharmacol Ther 2009, 123:54–79.

22. Möther H, Boisson D, Singer P, Feldon J, Pauly-Evers M, Yee BK: Glycine transporter 1 as a potential therapeutic target for schizophrenia. Curr Pharm Des 2011, 17:112–120.

23. Pasciacci J, Gentile G, Porter R, Herdon H, Salinas C, Jakobsen S, Audrain H, Laruelle M, Gunn RN: Identification and evaluation of [11C]GSK931145 as a novel ligand for imaging the type 1 glycine transporter with positron emission tomography. Synapse 2010, 64:542–549.

24. Hammil TG, Eng W, Jennings A, Lewis R, Thomas S, Wood S, Street L, Wosinski D, Wolkenberg S, Lindsay C, Sanabria-Botelhoque SM, Patel S, Riffel K, Ryan C, Cook J, Sur C, Burns HD, Hargreaves R: The synthesis and preclinical evaluation in rhesus monkey of [11C]MK-6577 and [11C]CMPyPB glycine transporter 1 positron emission tomography radiotracers. Synapse 2011, 65:261–270.

25. Gunn RN, Murthy V, Catarau AM, Searle G, Bullich S, Sifrelin M, Deuellet D, Zamuner S, Herance R, Salinas C, Pardo-Lozano R, Rabiner EA, Fare M, Laruelle M: Translational characterization of [11C]GSK931145, a PET Ligand for the glycine transporter type 1 (GlyT-1). Synapse 2011, 65:1319–1332.

26. Deportore R, Dargazanli G, Estenne-Bouhou G, Coste A, Laneau C, Desvignes C, Poncet M, Heulme M, Santucci V, Decobert M, Cudennec A, Voltz C, Boulay D, Terranova JP, Stemmlin J, Roger P, Marabou B, Sevrin M, Veiga X, Biton B, Steiner G, Françon D, Alonso R, Avenet P, Oury-Donat F, Perrault G, Giebel G, George P, Sourbrie P, Scallon B: Neurochemical, electrophysiological and pharmacological profiles of the selective inhibitor of the glycine transporter-1 SRS504734, a potential new type of antipsychotic. Neuropsychopharmacology 2005, 30:1963–1985.

27. Toyohara J, Ishiwata K, Sakata M, Wu J, Nishiyama S, Tsukada H, Hashimoto K: In vivo evaluation of carbon-11 labelled non-sarcosine-based glycine transporter 1 inhibitors in mice and conscious monkeys. Nucl Med Biol 2011, 38:517–527.

28. Fuchigami T, Haratake M, Magata Y, Haradahira T, Nakayama M: Synthesis and characterization of [11C]Iodo-N-[5-(S)-(S)-1-methylpipеридин-2-yl](phenyl)methyl-3-trifluoromethyl-benzamide as novel imaging probe for glycine transporter 1. Bioorg Med Chem 2011, 19:6245–6253.