Microshear Bond Strength of Composite Resin to Enamel Treated With Titanium Tetrafluoride and the Carbon Dioxide Laser (10.6 µm): An In Vitro Study

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Abstract

Introduction: The present study aims to assess the microshear bond strength (µSBS) of composite to enamel treated with titanium tetrafluoride (TiF₄) and CO₂ laser irradiation.

Methods: Fifteen human molars were sectioned and their enamel surfaces were abraded. The sections were randomly assigned to 5 groups (n = 15): (CO); control group, (AP); treated with 1.23% acidulated phosphate fluoride (APF) for 4 minutes, (Ti); 4% TiF₄ for 1 minute, (L+AP); CO₂ laser irradiation (10.6 µm wavelength, 1 W peak power, 10 ms pulse duration, 500 ms repetition time, 0.2 mm beam spot size at the tissue level, 2 cm distance of handpiece tip to tissue surface (DSE, South Cores) followed by 1.23% APF, and (L+ Ti); 10.6μm CO₂ laser irradiation followed by 4% TiF₄ for one minute. Using Tygon tubes, Z250 (3M/ESPE) composite was bonded to the surface of the samples. The µSBS of composite to enamel was measured using a microtensile testing machine after 500 thermal cycles. The data were analyzed by one-way ANOVA and the Tukey HSD test (P<0.05).

Results: The mean µSBS was 20.66, 20.21, 13.44, 23.01, and 10.16 MPa in CO, AP, Ti, L+AP, and L+Ti groups respectively. Significant differences were observed between CO and Ti (P=0.026) and also CO and L+ Ti (P<0.0001).

Conclusion: The application of TiF₄ per se and after CO₂ laser irradiation on enamel decreased the µSBS of composite to enamel; on the other hand, APF alone and after laser irradiation did not have any adverse effect on the µSBS of composite to enamel.

Keywords: Acidulated phosphate fluoride; CO₂ lasers; Composite resins; Strength; Titanium tetrafluoride.

Introduction

Tooth decay is an infectious disease during which dental hard tissue is demineralized by the action of acids produced by the metabolism of cariogenic bacteria. If this process is stopped early enough, remineralization may occur. Several methods have been recommended for caries prevention such as fissure sealant therapy, the application of fluoride compounds and antimicrobial agents and laser irradiation.

Fluoride plays an important role in caries prevention. Fluoride is available in the forms of gel, varnish and solution for topical application. The mechanism of the action of fluoride is via the enhancement of remineralization and prevention of tooth demineralization. Different compositions of fluoride such as sodium fluoride (NaF), stannous fluoride (SnF₂), amine fluoride (AmF) and acidulated phosphate fluoride (APF) are used for caries prevention. The APF is an acidic compound which not only enhances the reaction of fluoride with enamel hydroxyapatite crystals by superficial demineralization, but also increases the concentration of phosphate and fluoride ions at the reaction site and prevents the development of caries. A new fluoride compound, titanium tetrafluoride (TiF₄), has recently been introduced to the market and is non-toxic with no reported complications so far. The optimal cariostatic...
efficacy of TiF₄ is attributed to the replacement of calcium in the composition of hydroxyapatite and the formation of titanium phosphate complexes.³

Titanium reacts with oxygen in water or hydroxyapatite and forms TiO₂, which confers acid resistance and enhances fluoride uptake by the enamel. Titanium dioxide forms a transparent glaze-like, non-globular layer on the tooth surface.³ Evidence shows that this transparent layer can increase the mineral content of enamel¹ and serve as a fluoride ion reservoir. Greater fluoride uptake following the application of TiF₄ is due to the bond of fluoride and metal ions to hydroxyapatite crystals. Due to the greater absorption of this particular fluoride compound compared to other forms, it has higher efficacy. Also, given that the smear layer is eliminated due to the highly acidic nature of TiF₄,³ it can penetrate into dentin and form a granular layer on the surface of dentin, decreasing dentin hypersensitivity.⁴ Moreover, TiF₄ has antimicrobial properties and prevents bacterial colonization.⁴

TiF₄ has a low pH and high affinity for a bond to oxygen atoms in a phosphate group; it forms a strong bond to the enamel surface as such.⁹ After the application of TiF₄,³ titanium compounds containing –Ti-O-Ti-O–chains are formed on the tooth surface⁸ and a strong complex is formed between the titanium compounds and hydroxyapatite. This theory regarding the bond of titanium reaction products to enamel is highly likely; however, it was maintained that the validity and nature of this bond must be further assessed.

Lasers have also been suggested for caries prevention.⁹ The wavelength of the CO₂ laser matches the absorbance spectrum of hydroxyl and phosphate groups in enamel hydroxyapatite crystals (9-11 μm). Thus, it is well absorbed only by the tooth surface without any adverse effect on pulp and can prevent dental caries. It enhances the efficacy of fluoride and increases fluoride uptake by the enamel. It prevents enamel demineralization and facilitates the conversion of hydroxyapatite to fluorapatite.¹⁰,¹¹ It also improves the cariostatic efficacy of fluoride-containing compounds such as NAF, APF and AmE. However, a few studies have been conducted regarding the effects of the combination of the CO₂ laser and TiF₄.¹²

Rodriguez et al. in 2004 evaluated the efficacy of the CO₂ laser for caries prevention in enamel and dentin and assessed its effect in combination with fluoride.¹³ They showed that CO₂ laser irradiation in different wavelengths modified the hydroxyapatite crystals and changed their reaction to acid attack.

In addition, CO₂ laser irradiation with fluoride had greater efficacy in the prevention of caries-like lesions compared to their use alone.¹⁴ In contrast, some studies reported that there was no significant difference between the outcomes of the irradiation of lasers before or after fluoride therapy.¹⁴ Topical applications of fluoride could a) promote enamel resistance to caries due to the less solubility of enamel in acidic conditions and b) prevent enamel decalcification.¹⁵ The application of fluoride results in the formation of fluorapatite deposits and may negatively affect the bond strength between enamel and composite resin material.¹⁶-¹⁸

This in vitro study aimed to evaluate the micro-shear bond strength (µSBS) of composite resin material to enamel treated with TiF₄ and the CO₂ laser. The null hypothesis was that the µSBS of composite resin material to enamel would not be significantly different after various surface treatments for caries prevention.

Materials and Methods

This in vitro experimental study was conducted on 15 extracted human sound molars which were stored in 1% saline until the experiment. The sample size was calculated to be 15 in each group considering the expected difference of mean µSBS among the four groups to be 8, 10, 15 and 20 MPa and standard deviation of 9 according to a previous study.¹⁹ The effect size of 0.52, the study power of 90%, and α = 0.05 in conjunction with Power Analysis and Sample Size software version 14 (PASS) were used to calculate the sample size (Total = 75).

The teeth were free from caries and surface defects such as cracks. After disinfection using 1% thymol solution, the teeth were sectioned into five slices by a cutting machine (Mecatome T201A, Persi, Germany) and each slice was mounted in red dental wax. The convex enamel surface was ground by 600-grit silicon carbide abrasive papers under water coolant to achieve a smooth and flat enamel surface for bonding to the composite and bond strength testing. Vinyl tape with a hole in it (2 mm diameter) was fixed on the abraded enamel surface for the purpose of standardization. Each slice was randomly allocated to one group as follows:

CO: No treatment (control group), AP: 1.23% APF gel was applied over the surface of samples for four minutes and was rinsed and dried, Ti: 4% TiF₄ was applied over the surface of samples for one minute and was rinsed and dried, and L+AP: the CO₂ Laser (DSE, South Korea) (Figure 1A) was irradiated on the surface of samples followed by the application of 1.23% APF gel for 4 minutes.

The TiF₄ gel with pH=1.2 was prepared by the dissolution of 4 g of TiF₄ powder (Aldrich Chemical Company, Milwaukee, WI, USA) in 100 mL deionized water and the addition of carboxymethyl cellulose immediately before the application.

The samples were then rinsed and dried. Laser parameters (Figure 1B) included 10.6 μm wavelength, pulse mode, 1 W power peak, 0.2 W average power, 64 W/cm² power density, 10 ms pulse width, 1 Hz frequency, 500 ms interval time, 10 seconds exposure time in a scanning movement, 640 W/cm² energy density, 0.2 mm spot size at the tissue level, and 2cm distance of handpiece tip from the surface. The irradiation was in a pulsed mode. The L+Ti: CO₂ laser was irradiated on the surface of samples as in the L+AP group followed by the application of 4%
TiF₄ gel for one minute. The samples were then rinsed and dried. Laser irradiation was carried out by a skilled operator who was blind to the study design and the laser was irradiated for 10 seconds in a scanning movement. All the materials were used according to the manufacturers’ instructions.

The teeth were then stored in artificial saliva until the bonding procedure. The surface of samples was etched with 37% phosphoric acid for 15 seconds (3M ESPE, St. Paul, MN, USA) according to the manufacturer’s instructions, rinsed and dried. Two-step etch and rinse adhesive, single bond, (3M ESPE, St., Paul, MN, USA) was then applied and light-cured with a LED light-curing unit (Demetron LC, Kerr, USA) for 20 seconds (600 mW/cm²). A Tygon tube (0.7 × 2 mm) was placed on the surface of samples and filled with the Z250 micro-hybrid composite (3M ESPE, St. Paul, MN, USA). The samples were light-cured for 40 seconds, stored for 24 hours and subjected to 500 thermal cycles between 5-55°C prior to µSBS assessment. Specimens were tested in a microtensile testing machine (Bisco, Livonia, MI, USA) with a crosshead speed of 0.5mm/min. The load at failure was recorded in Newton (N) and divided by the surface area in mm² to yield the µSBS value in MPa.

Statistical Analysis
The data were analyzed using SPSS version 22. The Kolmogorov-Smirnov test was applied to assess the normal distribution. One-way ANOVA was applied to detect the differences in µSBS. The Tukey HSD test was used for pairwise comparisons and P<0.05 was considered statistically significant.

Results
The mean, standard deviation (SD), maximum and minimum µSBS values of the composite to enamel in different groups are presented in Table 1. The mean ± SD of µSBS was 20.66 ± 7.94, 20.21 ± 3.49, 13.44 ± 5.29, 23.01 ± 9.38 and 10.16 ± 4.43 MPa in CO, AP, Ti, L+AP and L+Ti groups respectively. The Kolmogorov-Smirnov test revealed that the data were normally distributed. According to one-way ANOVA, significant differences were noted among the five groups in µSBS (P<0.05). Thus, the Tukey HSD test was applied for pairwise comparison of the groups. It revealed that the groups treated with APF either with laser irradiation or alone showed no significant differences with the control group. Significant differences were observed between the groups treated with TiF₄ and all other groups whether used in conjunction with laser irradiation or not (P<0.05). In fact, a significant reduction was detected when TiF₄ was applied. Therefore, the null hypothesis was rejected. The results of pairwise comparisons are shown in Table 2.

Discussion
Mechanical retention plays an important role in the adhesion of the composite to prepared enamel surfaces. The penetration of resin tags into microscopic pores and their mechanical interlocking plays an important role in the formation of a strong bond. This study was conducted to investigate the combined effect of TiF₄ and CO₂ laser application on the bond strength of composite resin to enamel.

The results of the present study showed that the application of TiF₄, either with or without CO₂ laser irradiation resulted in significantly lower bond strength. Reduction in µSBS following the application of fluoridated agents was attributed to the deposition of crystals, which are acid-resistant and may physically or chemically prevent complete penetration of adhesive resin. Sheykholeslam et al showed complete degradation of the resin bond to bovine enamel following the application of TiF₄ for five minutes. It was proposed that acid-resistant globular deposits are the main cause of the reduction in

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**Table 1.** The Mean (MPa), Standard Deviation, Maximum and Minimum Shear Bond Strength Values of the Composite to Enamel of the Study Groups

| Group Name | Mean  | SD    | Minimum | Maximum |
|------------|-------|-------|---------|---------|
| CO         | 20.66 | 7.94  | 9.90    | 36.20   |
| AP         | 20.21 | 3.49  | 14.20   | 27.30   |
| Ti         | 13.44 | 5.29  | 7.50    | 27.70   |
| L+AP       | 23.01 | 9.38  | 9.10    | 38.80   |
| L+Ti       | 10.16 | 4.43  | 3.60    | 18.50   |

**Table 2.** Pairwise Comparison of the Groups Using the Tukey HSD Test

| Group 1 | Group 2 | P Value |
|---------|---------|---------|
| CO      | L+AP    | 0.859   |
|         | AP      | 1.00    |
|         | Ti      | 0.026   |
|         | L+Ti    | 0.000   |
| L+Ti    | Ti      | 0.641   |
|         | L+AP    | 0.000   |
|         | AP      | 0.001   |
| L+AP    | Ti      | 0.001   |
|         | AP      | 0.763   |
| AP      | Ti      | 0.044   |
bond strength since they inhibit resin tag formation and decrease the wettability of enamel.

Evidence shows the fast formation of compounds by the reaction of TiF$_4$ or its derivatives with phosphate or organic contents of dentin.$^{24}$ A glaze-like layer is formed, which is referred to as the organometallic complex. This complex forms a strong titanium-rich coating on the tooth surface, which is stable against acidic and alkaline wear.$^{24,25}$ The presence of a strong coating with 0.1 µm thickness has been reported on surfaces treated with TiF$_4$.$^{26}$ Another study reported the presence of a glaze-like layer on the occlusal surface of posterior teeth for up to one year following the application of TiF$_4$.$^{27}$

As it was mentioned earlier, a further decrease in bond strength was observed when TiF$_4$ was used in conjunction with the CO$_2$ laser. It was maintained that TiF$_4$ requires organic groups to form organometallic complexes on the tooth surface.$^{16,17}$ After laser irradiation, the organic content of the enamel surface decreases. Apatite crystals fuse and form a more mineralized structure. It appears that TiF$_4$ can no longer affect the surface, and the laser-modified smooth surface cannot be well-etched to form micromechanical bonds with adhesive resin.

The glaze-like layer on the surface (which prevents adequate tooth surface preparation by phosphoric acid) can form chemical bonds with the adhesive depending on the acidity and composition of the adhesive used. This explains the further reduction in bond strength in the laser plus TiF$_4$ group compared to TiF$_4$ alone. Further studies are required to investigate the optimal etching time for enamel after tooth conditioning with TiF$_4$.

One possible mechanism for the acquired acid-resistance by laser-irradiated enamel is via the formation of small empty spaces, which serve as a place for the entrapment and storage of mineral ions released during the acid attack; however, in non-laser irradiated enamel, the ions are released into the surrounding solution. This theory explains enamel resistance to acid following laser irradiation.$^{28}$ Another suggested mechanism is the formation of pyrophosphate following CO$_2$ laser irradiation; the CO$_2$ laser melts and recrystallizes enamel and dentin.$^{12}$ Laser irradiation of enamel causes superficial melting and solubilizes the crystalline structure, followed by recrystallization in the presence of fluoride and formation of fluorapatite, which is less soluble than hydroxyapatite.$^{29}$

Based on the results of the current study, irradiation of the CO$_2$ laser prior to the application of APF has not exhibited an increase in bond strength compared to that of APF alone. It appears that surface recrystallization due to laser irradiation confers resistance to enamel against acid etching and thus decreases bond strength. However, the application of APF results in the deposition of calcium fluoride globules on the tooth surface, which increase surface porosity and enhance the mechanical retention of adhesive and consequently a higher bond strength.$^{30}$ but the durability of this bond in the long term needs to be evaluated in future studies.

In the current study, the µSBS of the composite to enamel following the application of APF with/without CO$_2$ laser irradiation was higher than that of TiF$_4$ groups. Contrary to TiF$_4$, APF cannot form an organometallic complex and only forms globular calcium fluoride deposits on the tooth surface, which do not adhere to the surface as strongly as the glaze-like layer formed by TiF$_4$ and cannot perform as a strong barrier against the adequate bond of the composite to the tooth surface.$^{11,32}$

To have a more comprehensive study, TiF$_4$ had to be compared with other fluoridated compounds. Moreover, different laser parameters had to be used, SEM analysis had to be conducted and the procedure had to be carried out over an extended period of time. However, due to some limitations, the study was confined to its present form.

**Conclusion**

The application of TiF$_4$ alone and after CO$_2$ laser irradiation on the enamel surface decreased the µSBS of the composite to enamel. APF alone or its use after laser irradiation did not have any adverse effect on the µSBS of the composite to enamel.

**Ethical Considerations**

Not Applicable.

**Conflict of Interests**

The authors declare no conflict of interest.

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