Abstract
Several studies related to emotion recognition based on Electroencephalogram signals have been carried out in feature extraction, feature representation, and classification. However, emotion recognition is strongly influenced by the distribution or balance of Electroencephalogram data. On the other hand, the limited data obtained significantly affects the imbalance condition of the resulting Electroencephalogram signal data. It has an impact on the low accuracy of emotion recognition. Therefore, based on these problems, the contribution of this research is to propose the Radius SMOTE method to overcome the imbalance of the DEAP dataset in the emotion recognition process. In addition to the EEG data oversampling process, there are several vital processes in emotion recognition based on EEG signals, including the feature extraction process and the emotion classification process. This study uses the Differential Entropy (DE) method in the EEG feature extraction process. The classification process in this study compares two classification methods, namely the Decision Tree method and the Convolutional Neural Network method. Based on the classification process using the Decision Tree method, the application of oversampling with the Radius SMOTE method resulted in the accuracy of recognizing arousal and valence emotions of 78.78% and 75.14%, respectively. Meanwhile, the Convolutional Neural Network method can accurately identify the arousal and valence emotions of 82.10% and 78.99%, respectively.

Keywords:
Electroencephalogram; Radius-SMOTE; Emotion Recognition; Oversampling; Imbalance Data.

1- Introduction

Emotions are a conscious or unconscious human perception of an object capable of triggering psychological processes such as mood, anger, personality, self-efficacy, and motivation [1–3]. Several studies have examined the recognition of human emotions both internally and externally. For instance, studies by [4–12] stated that external human emotions can be recognized through text, facial expressions, body movements, and speeches. However, the external emotional expression is usually deliberately hidden in the social environment, which makes the recognition not optimal [13–15]. On the other hand, the recognition process can be conducted using Autonomous Neural Systems (ANS), such as Galvanic Skin Responses (GSR), Respiration (RSP), and Electrocardiogram (ECG) [16–20]. Meanwhile, the recognition through ANS is very sensitive to several disorders, such as skin diseases and physical activity. Various human activities also produce signals similar to emotional states, which tend to affect emotion recognition accuracy. Therefore, the use of
physiological signals from the Central Nervous System (CNS) via Electroencephalogram (EEG) can solve this problem due to its ability to easily represent emotional reactions [21]. EEG signals have spatial, temporal, and spectral information related to human affective experience. Subsequently, it is easy to install and use to record emotions [21–23].

Several studies have analyzed human emotion recognition, based on EEG signals, in data acquisition, feature extraction, and emotion classification [14, 23–27]. However, emotion recognition is strongly influenced by the distribution or balance of Electroencephalogram data [28]. Conversely, the limited data obtained significantly affects the imbalance condition of the resulting Electroencephalogram signal data. It impacts the low accuracy of emotion recognition [29]. Although some emotion data, such as the DEAP dataset, are publicly available, this data set has an uneven distribution, causing imbalance problems in the high and low classes [20, 30]. Similarly, the imbalanced dataset can influence accuracy performance on emotion recognition.

There are several advantages of the Radius SMOTE method compared to other oversampling methods, such as the ability to overcome the problem of dataset imbalance. The Radius SMOTE method can overcome overlapping, small displacement, and noise when synthesizing new data [31–33]. Furthermore, it has also been successfully applied in the oversampling process of fetal umbilical cord image data and has increased accuracy [33]. Therefore, based on these problems, this study proposes a Radius SMOTE method to overcome the imbalance of the DEAP dataset in the emotion recognition process.

The entire study is organized into four sections, where Section 1 introduces the study. Section 2 presents the related work of the oversampling study. Section 3 offers an emotion recognition theory and method using an oversampling data approach. Section 4 presents the experiment results, discussion, and limitations of these studies—finally, Section 5 offers the conclusion and the limitations of these studies and contributions for further investigation.

2- Literature Review

The oversampling process is used to create new synthetic data for the minority class due to its ability to improve classification accuracy than the under-sampling process [34]. There are two oversampling strategies, namely random and synthetic. Random oversampling is a non-heuristic method used to add data to a small portion of minor classes [33, 35, 36]. Ding et al. (2021) [36] conducted an oversampling study using the Random Oversampling method for the DEAP dataset. This method increased the accuracy of the recognition of arousal and valence emotions. However, it tends to experience overfitting problems [33]; hence it is imperative to generate new synthetic data from minority classes based on neighboring locations. Making synthetic data can use the Synthetic Minority Oversampling Technique (SMOTE) to overcome the overfitting problem found in the Random Oversampling method.

Several studies have been carried out using the SMOTE method to overcome data imbalance. For instance, the study by Sanguanmak and Hanskunatai (2016) [37] on using the SMOTE method for oversampling minor class data by combining oversampling and under-sampling techniques. Morales et al. (2013) [38] studied the use of Synthetic Oversampling of Instance Clustering (SOI-C) and Synthetic Oversampling of Instance Jittering (SOI-J). This approach compares the minor class data in each cluster during the synthetic data creation process with the MWMOTE method used to select sample data developed by Barua et al. (2014) [39]. In this study, each minor class data was given a weighted value based on the number of k Nearest Neighbor of the majority class data. The grouping process was carried out the Safe-Level-SMOTE method proposed by Bunkhumpornpat et al. (2009) [40] to avoid overlapping synthetic data in the minority class. This strategy was used to modify the SMOTE method by adding an initial selection process before creating new synthetic data.

However, several inconsistencies are associated with the SMOTE method, such as overlapping, small disjunct, and noise. Overlap is a condition in which some minority and majority class data distributions have the same area. Small disjunct is a condition where the majority class mainly surrounds the distribution of the minority. Meanwhile, noise is the process whereby the majority class covers the sample of the minority data. This condition can complicate the classification method responsible for determining the decision limit for each category [32, 41]. Therefore, based on this problem, the Radius SMOTE method can overcome its weaknesses due to its ability to produce synthetic data from minor classes on the image of the fetal umbilical cord. The oversampling process can improve classification accuracy on fetal umbilical cord image data [33]. Based on these problems, this study proposes the Radius SMOTE method for the imbalance oversampling process in the DEAP dataset. In addition to the EEG data oversampling process, there are several vital processes in emotion recognition, such as the feature extraction and the emotion classification processes using the Differential Entropy (DE) method. According to [42], the method is capable of characterizing spatial data from EEG signals with the highlights feature comprising foremost exact and steady features [28, 43–46]. The classification process in this study compares two methods, namely the Decision Tree and the Convolutional Neural Network. The purpose of applying these two classification methods is to measure the accuracy of EEG data oversampling performance on a machine and deep learning.
3- Methodology

This chapter discusses several stages of the oversampling approach using the Radius SMOTE method for emotion recognition, as shown in Figure 1.

![Diagram](image)

**Figure 1. EEG signal-based emotion recognition flowchart**

Figure 1 shows seven stages in emotion recognition, namely the preprocessing, feature extraction, oversampling (which is the contribution of this study), feature representation, classification, validation, and accuracy calculation stages.

3-1- DEAP Dataset

The dataset used in this study is the DEAP. This dataset is publicly accessible via the web [https://www.eecs.qmul.ac.uk/mmv/datasets/deap/](https://www.eecs.qmul.ac.uk/mmv/datasets/deap/). The following is a description of the DEAP dataset [20]:

- The EEG signal data collected in this dataset consists of thirty-two participants with an equal number of males and females within the age of 19-37 years.
- These emotional reactions are recorded using an EEG device called Biosemi, where the number of channels used amounted to thirty-two.
- A total of 40 experiments with stimulus media for each participant were used to evoke their emotional reactions.
- The duration for each experiment is 1 minute (60 seconds), while the total time of the investigation per participant was 2400 seconds (40 experiments × 60 seconds).
- Every second for each channel of the EEG device produces an EEG sampling rate of 128 Hz.

In the DEAP dataset, the EEG signal acquisition process is carried out by placing thirty-two channels on the scalp. The position of the thirty-two channels on the scalp is presented in Figure 2.

![Diagram](image)

**Figure 2. The positioning of the 32 channels on the scalp is based on the System 10-20 International standard**
In Figure 2, NASION represents the skull’s front, precisely at the top center of the forehead, while INION denotes the lower back. Meanwhile, Fp, F, T, P, O, and C represents the prefrontal, frontal, temporal, parietal, occipital, and central head. In addition, the following channels represent the development of several existing channels:

- AF is a channel placed between Fp and F;
- FC is a channel placed between F and C;
- CP is a channel placed between C and P;
- PO is a channel placed between P and O.

The position of channel placement in this DEAP dataset uses the 10–20 International standard system. These values represent the percentage (%) of the distance between NASION and INION channels. Standard procedures have been carried out in the DEAP dataset acquisition process, starting from determining stimulus media, proper presentation setup, and standardization of experimental protocols. However, this dataset has data imbalance conditions found in participants S01, S02, S03, S04, S07, S09, S11, S12, S13, S14, S17, S18, S19, S20, S21, S22, S23, S24, S25, S27, S29, and S32. These unbalanced data are relatively high (40% < not balanced between high and low classes) on arousal emotion. Participants S04, S05, S06, S07, S11, S16, S18, S23, S26, S27, S28, and S30 had unbalanced data conditions, which were relatively high (40% < not balanced between high and low classes) on valence emotions. However, participants S16 had a balanced dataset condition for arousal emotion, while S09, S10, S14, S15, and S32 are associated with valence emotion. In addition to these participants, some participants had an imbalance condition that was not too high [20]. Therefore, this study proposes the Radius SMOTE method for oversampling the imbalance data in the DEAP dataset.

3.2- Preprocessing

At this stage, the decomposition process using a bandpass filter is carried out to determine the four frequencies of the EEG signal for the 32 channels. A bandpass filter is used to decompose the EEG signal on each channel into four frequency bands, namely Theta, Alpha, Beta, and Gamma frequencies. The decomposition process is carried out by determining each frequency band’s Low and High Pass values. Table 1 shows the respective Low Pass and Band Pass values for each frequency band [28, 46, 47].

| Frequency band | Low Pass | High Pass | Brain state                      |
|---------------|----------|-----------|----------------------------------|
| Gamma (γ)     | 35 Hz    | 45 Hz     | Concentration                    |
| Beta (β)      | 12 Hz    | 35 Hz     | Anxious, active, outwardly attentive, relaxed |
| Alpha (α)     | 8 Hz     | 12 Hz     | Passive attention                |
| Theta (θ)     | 4 Hz     | 8 Hz      | Very relaxed, focused inward.    |

In general, the EEG signal has five frequency bands, out of which four, namely Theta, Alpha, Beta, and Gamma, are correlated with emotional reactions [46, 48]. Figure 3 shows the decomposition process of the EEG signal into four frequency bands for the Fp1 and O2 channels. However, this process is carried out on all 32 channels, followed by the segmentation process in all sixty segments for each frequency band consisting of 32 participants. In the DEAP dataset, a participant was expected to conduct forty experiments. Figure 4 shows the segmentation process on the Frontopolar 1 (Fp1) and Occipital 2 (O2) channels for the first experiment.
The Fp1 and O2 channels produce sixty segments (Sg1 – Sg60) for one experiment. Each segment/piece consists of a 128 Hz sampling rate, while each participant is expected to possess 7680 segments (60 segments x 32 channels x 4 frequency bands).

3-3- Feature Extraction

After the segmentation process, the feature extraction process is carried out for each segment using the DE method. Each participant will generate 7680 DE feature data (32 channels x 4 frequency bands x 60 segments). Therefore, for the overall experiment, a total of 307200 DE feature data (7680 feature x 40 experiments) is obtained. The following is the formula for the Differential Entropy (DE) method [28, 46]:

\[
h_i(X) = \frac{1}{2} \log(2\pi e\delta^2)
\]

where \(e\) denotes Euler’s constant (2.71828), \(\delta^2\) represents variance, \(h_i\) is the Differential Entropy (DE) value corresponding to the EEG signal in each frequency band.

3-4- Oversampling

Radius-SMOTE is a method of making synthetic data by changing several steps. It is used to overcome problems, such as overlapping and noise, and also to decrease the accuracy performance in the classification process. Furthermore, it is also used to determine the imbalanced data, noise, and overlapping conditions in determining decision boundaries for each class in the dataset. In general, there are two stages of oversampling the EEG signal feature data from the minority class, namely the filtering and the synthetic data formation stages [33]:

- Filtering stage. At this stage, the selection process is carried out to obtain data from the right EEG feature (SAFE) using a radius approach divided into SAFE and NOISE data using the KNN algorithm. Furthermore, data in the SAFE category is used as a reference in oversampling new/synthetic data to reduce its occurrence and create new noise data. Data oversampling is limited to this circular area to avoid overlapping conditions to other class areas. Radius is used to determine the distance of the nearest majority data point from the sample and use it as the radius value. All new data points are created only within that radius constraint.

\[
\| b - p \| \leq r^2
\]

\[
\| g - p \| \leq r^2
\]

\[
\sum_{i=1}^{n}(b_{ij} - p_{ij})^2 \leq r^2
\]

where \(p_j\) (\(p_1, p_2, p_3, ... p_n\)) is the center point of the circle in the minority sample, while \(b_j\) (\(b_1, b_2, b_3, ... b_n\)) is the new data point in the radius. Next, the calculation process of \(r^2\) is calculated to determine the value of the distance between \(p_j\) and \(t_i\) as in Equation 5. The illustration of this proposed model is shown in Figure 5.

\[
r^2 = \sum_{j=1}^{n}(p_j - t_i)^2
\]
where \( t_i (t_1, t_2, t_3, \ldots, t_n) \) is the closest majority point to the center of the circle \((p_j)\). Furthermore, the distance of each minority sample is calculated from the majority class using the Euclidean distance method. The closest majority data point has a minimum distance to the minority data point, as shown in Equation 6.

\[
 r_{ij} = \min \sum_{i=1}^{n} \sum_{j=1}^{n} (p_j - t_i)^2
\]  

(6)

In this study, the Radius-SMOTE parameter uses the \( k \) value of 5 in the KNN method to perform the filtering process of sample data.

- EEG feature data creation stage. Making this synthetic data is based on the concept of radius, where the determination of the safe radius value is obtained from the circle equation. Its diameter is the distance between the EEG feature data of the SAFE category and the closest majority. Where \( r_{ij} \) is the smallest distance between the minority \((j)\) and majority \((i)\). After determining the majority of the data points, the formation of synthetic data is carried out by interpolating the two points. Synthetic data formation is carried out in two directions, namely \( r_{ij} \) (positive) and \(-r_{ij}\) (negative), with Equations 7 and 8:

\[
 a_{ij} = p_j + (\text{rand}(0,1) \times (r_{ij} - p_j)) 
\]  

(7)

\[
 b_{ij} = p_j + (\text{rand}(0,1) \times (p_j - r_{ij})) 
\]  

(8)

Limiting the area of creating new data reduces the occurrence of overlapping data in the SMOTE method [33]. Figure 5 shows the process of oversampling data using the Radius SMOTE method.

Furthermore, the amount of synthetic data is made based on the imbalanced ratio value in each dataset. Therefore, the higher the imbalanced ratio value, the greater the number of synthetic data formed in one sample data.

3-5- Feature Representation

Feature values for each experiment in four frequency bands are represented in a \( 9 \times 9 \) matrix. The blue, green, yellow, and red matrix denotes the theta, alpha, beta, and gamma-band frequencies. The combination of the four matrices is called the 3D Cube [46]. The DE feature values for all channels in each frequency band in one segment are represented in a \( 9 \times 9 \) matrix. Furthermore, the obtained matrix from the four frequency bands in one segment forms a 3D Cube representation. Figure 6 shows the 3D Cube representation method.
Figure 6 illustrates that there are 2400 3D Cube data (60 segments × 40 experiments) for one participant. The CNN method uses the 3D Cube data as input in the emotion classification process.

**3-6- Classification Process**

This study applied the CNN and the Decision Tree methods to measure the accuracy of EEG data oversampling performance on the machine and deep learning processes. The CNN method uses a 3D cube in each segment as input data, producing high or low emotion outputs for each arousal and valence. Its architecture in this study adopted the study by Yang et al. (2017) [46], as shown in Figure 7.
In the CNN method, each participant (independent subject) is carried out in one stage for the Arousal and Valence classification processes. Figure 7 shows that there are four processes in the CNN method for emotion classification, namely the convolution, flatten, fully connected, and output stages as follows [46]:

- **The convolution stage.** It is divided into four: the 1st, 2nd, 3rd, and 4th convolutions. The 1st uses a $4 \times 4 \times 64$ filter, with the stride value, activation function, and zero padding is 1, ReLU, and SAME, respectively. This is in addition to a resulting feature map of $9 \times 9 \times 64$. The 2nd convolution uses a $4 \times 4 \times 128$ filter, with a stride value, activation function, and zero padding is 1, ReLU, and SAME, respectively. This is in addition to the resulting feature map of $9 \times 9 \times 128$. The third convolution uses a $4 \times 4 \times 256$ filter, with a stride value, activation function, and zero padding is 1, ReLU, and SAME, respectively. In this convolution, the resulting feature map is $9 \times 9 \times 256$. Finally, the fourth convolution uses a $1 \times 1 \times 64$ filter, with a stride value, activation function, and zero padding is 1, ReLU, and SAME, respectively. In this convolution, the resulting feature map is $9 \times 9 \times 64$. The following is Equation 9 of the convolution process:

$$FM[i,j,k] = \left( \sum_m \sum_n N[j-m,k-n]F[m,n] \right) + bF$$

(9)

The variable $FM[i]$ represents the matrix of feature map at the $i$th index, where $F$, $N$, $b$, $j$, and $m$ and $n$ denotes the filter matrix, input matrix, the bias on the filter, the feature map locations in the input matrix, and the location of the filter matrix.

- **Flatten stage.** The feature map generated from the 4th convolution is reshaped at this stage, thereby measuring 5184 neurons ($9 \times 9 \times 64$).

- **Fully connected stage.** In this process, 5184 neurons are fully connected to 1024 hidden layers. This hidden layer uses a dropout operation of 0.5 to prevent overfitting and speed up the learning process. Dropout is carried out by deactivating the neurons connected to the hidden layer. The neuron to be deactivated is randomly chosen at a probability value of 0.5. Furthermore, weighted addition is carried out on the active neurons. Equation 10 is used to determine the weighted addition from input to the hidden layer.

$$z_{in} = \sum_{j=1}^{n} X_j \ast W_{j,i} + b_{l,i}$$

(10)

The variable $z_{in}$ represents the output value resulting from the weighted summation process in the $i$th output layer. Meanwhile, $X_j, W_{j,i}, b_{l,i}$, and $n$ denote the node value of the $j$th input layer, weight value from the input to the hidden layer, bias value from the input to the hidden layer, number of nodes from the input to the hidden layer. Furthermore, the value of the variable $z_{in}$ is activated using the softmax method, as shown in Equation 12.
Outputs stage. Furthermore, 1024 neurons in the hidden layer will be connected to two output layers representing high or low for arousal and valence, respectively. At this stage, a weighted summation process is also carried out from the hidden layer to the output layer. Equation 11 is used to determine the weighted addition from hidden to the output layer.

\[ y_{in,i} = \sum_{j=1}^{n} Z_{j} \ast V_{j,i} + b_{2,i} \]  

The variable \( y_{in,i} \) represents the output value resulting from the weighted summation process in the \( i \)th output layer. Meanwhile, \( Z_{j}, V_{j,i}, b_{2,i}, \) and \( n \) denote the node value of the \( j \)th hidden layer, weight value from the hidden to the output layer, bias value from the hidden to the output layer, number of nodes from the hidden to the output layer. Furthermore, the value of the variable \( y_{in,i} \) is activated using the softmax method, as shown in Equation 12.

\[ \sigma(Z_{i}) = \frac{e^{z_{i}}}{\sum_{j=1}^{K} e^{z_{j}}} \]  

where \( \sigma, Z, e^{z_{i}}, \) and \( e^{z_{j}} \) represent the softmax activation value, the value of the input vector, the standard exponential function of vector input, number of emotion classes, and the standard exponential function of vector output, respectively. The activation results will produce an output value that represents the high or low class for each Arousal and Valence emotion.

In this model, the loss value calculation and update processes use the cross-entropy loss and the Adam Optimizer methods. Furthermore, several parameters such as the learning rate (1e-4), the epoch (75), and the batch size (128) were determined. The second experiment in this study used the Decision Tree method. The max_depth parameter consists of a Decision Tree method with a value of 20 without using 3D Cube as input data. This method was implemented using the python programming language obtained from https://github.com/ynulonger/DE_CNN [46].

3-7- Validation Process

The accuracy measurement process is carried out at this stage using the K-Fold Cross Validation method with a K-value of 10. Measurement of the accuracy of emotion recognition of arousal and valence is also carried out for all 32 participants [46].

According to Figure 8, a participant has 2400 data divided into ten sections. The first part is used for the validation process (K=1), where the first 240 data are used as test data (in the orange block), and from the 241st to 2400th data (2160 data in the blue block) used as data training. The second part is used for the second validation process (K=2), where the 241st to 480th data (240th data in the orange colour block) are used as a test, while the first 240 (blue colour block) and from the 481st to the 2400th (1920 data in the blue colour block) used as training data. This validation process is repeated ten times (K=10), where the last 240 data were used as testing (in the orange colour block) and the first 2160 data as training (in the blue block). This process is used to validate the model responsible for recognizing categories of arousal emotions.

\[ \text{K=1} \]

240 data

Testing data

2160 data

Training data

\[ \text{K=2} \]

240 data

Training data

240 data

Testing data

1920 data

\[ \text{K=10} \]

2160 data

Training data

240 data

Testing data

Figure 8. Illustration of the validation process using K-Fold Cross-Validation
3-8 Emotion Accuracy

The emotion category in this study refers to the Russell Circumplex model, where it can be grouped into arousal and valence, with each class consisting of high or low value. In theory, valence is an individual’s emotion towards something or an event. Meanwhile, arousal is an individual’s excitement to behave or express their emotions [49, 50]. Figure 9 presents an emotional representation based on the Russell Circumplex model.

![Russell Circumplex Model](image)

**Figure 9.** Russell circumplex model [51]

Each validation process produces an accuracy value for both arousal and valence emotions for the High/Low emotion category. The accuracy value of this study will be compared with emotion recognition from several preliminary studies. This comparison of accuracy aims to examine the proposals of this study.

4- Results and Discussion

This chapter presents the proposed Radius SMOTE method used for oversampling imbalanced data on the DEAP dataset. In Table 2, the DEAP dataset is presented for each imbalanced participant [20].

| No | Participants | Arousal data | Valence data | No | Participants | Arousal data | Valence data |
|----|--------------|--------------|--------------|----|--------------|--------------|--------------|
| 1  | S01          | 960 (low)    | 1140 (high)  | 17 | S17          | 960 (high)   | 1080 (high)  |
| 2  | S02          | 960 (low)    | 1080 (low)   | 18 | S18          | 900 (low)    | 960 (low)    |
| 3  | S03          | 480 (high)   | 1080 (low)   | 19 | S19          | 780 (low)    | 1020 (low)   |
| 4  | S04          | 960 (high)   | 960 (high)   | 20 | S20          | 540 (low)    | 1020 (low)   |
| 5  | S05          | 1140 (high)  | 960 (low)    | 21 | S21          | 480 (low)    | 1140 (low)   |
| 6  | S06          | 1020 (low)   | 600 (low)    | 22 | S22          | 960 (low)    | 1080 (high)  |
| 7  | S07          | 900 (low)    | 720 (low)    | 23 | S23          | 600 (high)   | 840 (low)    |
| 8  | S08          | 1020 (low)   | 1080 (low)   | 24 | S24          | 420 (low)    | 1080 (high)  |
| 9  | S09          | 960 (low)    | Balance      | 25 | S25          | 660 (high)   | 1140 (high)  |
| 10 | S10         | 1080 (low)   | Balance      | 26 | S26          | 1020 (high)  | 840 (low)    |
| 11 | S11         | 900 (high)   | 960 (low)    | 27 | S27          | 780 (low)    | 600 (low)    |
| 12 | S12         | 420 (low)    | 1140 (low)   | 28 | S28          | 1080 (high)  | 900 (high)   |
| 13 | S13         | 360 (low)    | 1020 (high)  | 29 | S29          | 900 (low)    | 1020 (low)   |
| 14 | S14         | 780 (high)   | Balance      | 30 | S30          | 1140 (high)  | 780 (low)    |
| 15 | S15         | 1140 (high)  | Balance      | 31 | S31          | 1140 (high)  | 1020 (low)   |
| 16 | S16         | Balance      | 900 (high)   | 32 | S32          | 780 (low)    | Balance      |
The DEAP dataset consists of balanced data for several participants. This data is obtained assuming there are high and low classes of arousal/valence with the same value of 1200 data, culminating in 2400 data. The distribution of the DEAP dataset after the oversampling process using Radius-SMOTE is shown in Table 3.

### Table 3. Distribution of minor class in DEAP dataset after oversampling

| No | Participants | Arousal data | Valence data | No | Participants | Arousal data | Valence data |
|----|--------------|--------------|--------------|----|--------------|--------------|--------------|
| 1  | S01          | 1607 (low)   | 1972 (high)  | 17 | S17          | 1648 (high)  | 1389 (high)  |
| 2  | S02          | 1526 (low)   | 1873 (low)   | 18 | S18          | 1434 (low)   | 1693 (low)   |
| 3  | S03          | 1680 (high)  | 1839 (low)   | 19 | S19          | 1572 (low)   | 1667 (low)   |
| 4  | S04          | 1820 (high)  | 1575 (high)  | 20 | S20          | 1788 (low)   | 1798 (low)   |
| 5  | S05          | 1916 (low)   | 1546 (low)   | 21 | S21          | 1920 (low)   | 1722 (low)   |
| 6  | S06          | 1688 (high)  | 1790 (low)   | 22 | S22          | 1920 (low)   | 1814 (high)  |
| 7  | S07          | 1464 (low)   | 1610 (low)   | 23 | S23          | 1929 (high)  | 1408 (low)   |
| 8  | S08          | 1716 (low)   | 1846 (low)   | 24 | S24          | 2100 (low)   | 1745 (high)  |
| 9  | S09          | 1603 (low)   | Balance      | 25 | S25          | 1788 (high)  | 1913 (high)  |
| 10 | S10         | 1967 (low)   | Balance      | 26 | S26          | 1671 (high)  | 1308 (low)   |
| 11 | S11          | 1572 (high)  | 1648 (low)   | 27 | S27          | 1678 (low)   | 2030 (low)   |
| 12 | S12          | 1815 (low)   | 2018 (low)   | 28 | S28          | 1795 (high)  | 1478 (high)  |
| 13 | S13          | 1965 (low)   | 1690 (high)  | 29 | S29          | 1457 (low)   | 1715 (low)   |
| 14 | S14          | 1722 (high)  | Balance      | 30 | S30          | 1964 (high)  | 1644 (low)   |
| 15 | S15          | 2071 (high)  | Balance      | 31 | S31          | 1988 (high)  | 1699 (low)   |
| 16 | S16          | Balance      | 1584 (high)  | 32 | S32          | 1820 (low)   | Balance      |

Table 3 indicates that the Radius-SMOTE method will generate synthetic data on the minor class. However, the addition of synthetic data exceeds the majority class, while data in the minority class becomes the majority after oversampling using Radius-SMOTE. This is followed by the classification process of deep and machine learning, using the CNN and Decision Tree methods. The use of these two methods aims to measure the results of emotion classification using deep and machine learning approaches. Based on the validation and classification processes using the K-Fold Cross-validation and the CNN methods, the accuracy values for recognizing arousal and valence emotions are 82.11% and 78.99%, respectively. Meanwhile, the accuracy value of using the Decision Tree method for the classification process, arousal, and valence accuracy is 78.78% and 75.14%, respectively. Figure 10 shows the accuracy of arousal emotion recognition for each participant using the CNN and the Radius SMOTE methods.

![Comparison graph of accuracy between balanced and imbalanced data on arousal](image.png)

**Figure 10.** Comparison of arousal accuracy for using CNN and with or without the Radius SMOTE method.
In Figure 10, the Radius SMOTE method for oversampling data and the CNN method for the classification process have the ability to increase the accuracy of recognizing arousal emotions. However, one participant with ID s16 did not show an increase in accuracy because the data was balanced, hence there was no oversampling. Subsequently, the Radius SMOTE and the CNN method are used to recognize valence emotions, as shown in Figure 11.

Figure 11. Comparison of valence accuracy for using CNN and with or without the Radius SMOTE method

Generally, using the Radius SMOTE method can improve the accuracy of recognizing valence emotions. However, some participants, such as ID s09, s10, s14, s15, and s32, did not experience an increase. However, the oversampling process was not carried out on these participants because the data was balanced. Apart from using the CNN method, this study also examined the use of the Decision Tree method combined with the Radius SMOTE. Figure 12 compares the accuracy with and without the Radius SMOTE method for recognizing arousal emotions.

Figure 12. Comparison of arousal accuracy for using Decision Tree and with or without the Radius SMOTE method
Figure 12 shows that the Radius SMOTE with the Decision Tree method increases the accuracy of recognizing arousal emotions. However, one participant with ID s16 did not experience an increase because the data were balanced without oversampling process. In the same way, the use of the Radius SMOTE method with the Decision Tree method can also increase the accuracy of recognizing valence emotions, as shown in Figure 13.

![Comparison graph of accuracy between balanced and imbalanced data on valence](image)

**Figure 13.** Comparison of valence accuracy for using Decision Tree and with or without the Radius SMOTE method

The Radius SMOTE method can improve recognizing valence emotions. However, some participants, such as ID s09, s10, s14, s15, and s32, did not experience an increase because of these data without oversampling process. In general, using Radius-SMOTE to oversampling on the DEAP dataset can improve emotion recognition accuracy. This conclusion indicates that the imbalanced data conditions in the DEAP dataset can reduce the accuracy of emotion recognition. Furthermore, the accuracy results obtained from this study are compared with several others, as shown in Table 4.

**Table 4. Comparison of emotion recognition accuracy in several studies**

| No | Studies | Model | Arousal | Valence |
|----|---------|-------|---------|---------|
| 1  | Yang et al. [46] | The Differential entropy method for feature extraction, The 3D Cube method for feature representation, and The CNN method for classification. | 69.55% | 68.56% |
| 2  | Yang et al. [46] | The Differential entropy method for feature extraction, and the Decision Tree method for classification. | 63.86% | 62.52% |
| 3  | Yang et al. (2018) [52] | Combination of the CNN method and the LSTM method for feature extraction and classification. | 61.78% | 57.05% |
| 4  | Chao et al. [48] | The Power Spectral Density method for feature extraction, the Multiband Feature Matrix method for feature representation, and the Capsule Network for classification. | 68.28% | 66.73% |
| 5  | Liu et al. [47] | The Multi-level feature method for feature representation and Capsule Network for classification. | 64.36% | 62.57% |
| 6  | Ding et al. [36] | The Dispersion Entropy method for feature extraction, The SVM method for classification, and Random Oversampling for oversampling data | 76.67% | 72.95% |
| 7  | Purpose study | The Differential entropy method for feature extraction, the Decision Tree method for classification, and the Radius-SMOTE method for oversampling data | 78.78% | 75.14% |
| 8  | Purpose study | The Differential entropy method for feature extraction, the 3D Cube method for feature representation, the CNN for classification, and the Radius-SMOTE method for oversampling data. | 82.11% | 78.99% |

The Radius SMOTE method for the oversampling process produces a higher arousal and valence emotion recognition accuracy than those proposed by Yang et al. in the DEAP data set [46]. Although the emotion classification process has been improved using the Capsule Network method and the combination of Convolutional Neural Network and Long Short Term Memory methods; however, the accuracy is achieved still lower than this research proposal [47, 48, 52]. On the other hand, the oversampling process on imbalanced data using the Radius SMOTE method produces higher accuracy.
than the Random Oversampling method [36]. In general, the application of the Differential Entropy, Radius SMOTE, 3D Cube, and Convolutional Neural Network for feature extraction, imbalanced data, representation, and classification in this study led to higher accuracy compared to some of the previous studies [36, 46–48, 52].

5- Conclusion

The problem of data imbalance in the DEAP dataset was solved by applying an oversampling approach using the Radius-SMOTE method. The oversampling process produces new synthetic data on the minority class. This study conducted two experiments to measure the Radius SMOTE method's ability to increase emotion recognition accuracy. The feature extraction process used the Differential Entropy and the Decision Tree methods for the classification process in the first experiment. The second experiment used the Differential Entropy, 3D Cube, and Convolutional Neural Network for feature extraction, representation, and emotion classification processes. Based on these two experiments, the oversampling approach using the Radius SMOTE method increases the accuracy of recognizing arousal and valence emotions. In essence, the Radius SMOTE is an oversampling method used to create new synthetic data based on secure Radius data. However, making synthetic data does not consider the amount of data in the majority class, thus causing the previously in the minority class to become the majority class. So the data will still experience an unbalanced condition. In the future, it is necessary to determine the suitable method to handle unbalanced data, both from the undersampling approach and other approaches.

Conversely, though emotion recognition accuracy has increased, it is still below 85% in arousal and valence. This problem becomes a challenge in future studies in recognizing emotions based on EEG signals. Therefore, emotion recognition based on EEG signals is strongly influenced by participant characteristics. Combining the baseline reduction approach to characterize participant characteristics is essential to examine the oversampling approach.

5-1- Limitations

The Radius SMOTE method is an oversampling method used to create new synthetic data based on SAFE radius data. However, its development does not consider the amount of data in the majority class; hence the minority class becomes the majority. In the future, it is necessary to determine the suitable method to handle unbalanced data, both from the under-sampling approach and other approaches. On the other hand, though emotion recognition accuracy has increased, the average accuracy is still below 85% for emotional arousal and valence. This problem becomes a challenge in future studies in its recognition based on EEG signals, which is strongly influenced by participant characteristics, such as personality traits, intellectual abilities, and gender [28, 53]. Therefore, further study needs to be conducted to examine the oversampling approach and allow the combination with the baseline reduction approach to characterize participant characteristics.

6- Declarations

6-1- Author Contributions

Conceptualization, R.W.; preparation of introduction, I.M.A.W.; preparation of related work, I.M.A.W. and I.G.A.P.; data collection and analysis, R.W. and I.M.A.W.; preparation of the preprocess methodology, R.W. and I.M.A.W.; compilation of methods and theory of feature extraction, R.W. and I.M.A.W.; compilation of theory and methodology Radius SMOTE, R.W. and I.G.A.P.; compilation of the theory and methodology of feature representation, R.W. and I.M.A.W.; compilation of the theory and methods of classification process, R.W. and I.M.A.W.; formulation of validation theory and methodology, R.W. and I.M.A.W.; compilation of theory and methods of accuracy measurement, R.W. and I.M.A.W.; development of oversampling technique using the Radius SMOTE method, I.G.A.P.; development of Differential Entropy method for feature extraction, I.M.A.W.; development of the 3D Cube method for feature representation, I.M.A.W.; development of the Convolutional Neural Network method and the Decision Tree method for the classification process, I.M.A.W.; preparation of results and discussion, R.W. and I.M.A.W.; drawing conclusions, R.W. and I.M.A.W. All authors have read and agreed to the published version of the manuscript.

6-2- Data Availability Statement

The data used in this study is the DEAP dataset. This dataset is freely accessible at [https://anaxagoras.eecs.qmul.ac.uk/request.php?dataset=DEAP].

6-3- Funding

The authors received no financial support for the research, authorship, and/or publication of this article.

6-4- Ethical Approval

Not applicable.
6-5- Conflicts of Interest

The authors declare that there is no conflict of interests regarding the publication of this manuscript. In addition, the ethical issues, including plagiarism, informed consent, misconduct, data fabrication and/or falsification, double publication and/or submission, and redundancies have been completely observed by the authors.

7- References

[1] Subramanian, R., Wache, J., Abadi, M. K., Vieriu, R. L., Winkler, S., & Sebe, N. (2018). Ascertain: Emotion and personality recognition using commercial sensors. IEEE Transactions on Affective Computing, 9(2), 147–160. doi:10.1109/TAFFC.2016.2625250.

[2] Setyohadi, D. B., Sri Kusrohmaniah, Christian, E., Dewi, L. T., & Sukci, B. P. (2017). M-Learning interface design based on emotional aspect analysis. Lecture Notes in Computer Science (Including Subseries Lecture Notes in Artificial Intelligence and Lecture Notes in Bioinformatics), 10127 LNCS, 276–287. doi:10.1007/978-3-319-52503-7_22.

[3] Daher, W., Baya’a, N., & Anabousy, A. (2021). Emotions and self-efficacy as mediators of pre-service teachers’ adoption of digital tools. Emerging Science Journal, 5(5), 636–649. doi:10.28991/esj-2021-01301.

[4] Seyeditabar, A., Tabari, N., & Zadrozy, W. (2018). Emotion Detection in Text: a Review. http://arxiv.org/abs/1806.00674

[5] Alsawai, N., & Menai, M. E. B. (2020). Hybrid Feature Model for Emotion Recognition in Arabic Text. IEEE Access, 8, 37843–37854. doi:10.1109/ACCESS.2020.2975906.

[6] Gunadi, I. G. A., Harjoko, A., Wardoyo, R., & Ramdhani, N. (2015). The extraction and the recognition of facial expression based on certainty factor. Journal of Theoretical and Applied Information Technology, 82(1), 113–121.

[7] Ko, B. C. (2018). A brief review of facial emotion recognition based on visual information. Sensors (Switzerland), 18(2). doi:10.3390/s18020401.

[8] Lamba, P. S., & Virmani, D. (2018). Information retrieval from emotions and eye blinks with help of sensor nodes. International Journal of Electrical and Computer Engineering, 8(4), 2433–2441. doi:10.11591/ijece.v8i4.pp2433-2441.

[9] Mehta, D., Siddiqui, M. F. H., & Javaid, A. Y. (2018). Facial emotion recognition: A survey and real-world user experiences in mixed reality. Sensors (Switzerland), 18(2), 1–24. doi:10.3390/s18020416.

[10] Salmam, F. Z., Madani, A., & Kissi, M. (2018). Emotion recognition from facial expression based on fiducial points detection and using neural network. International Journal of Electrical and Computer Engineering, 8(1), 52–59. doi:10.11591/ijece.v8i1.pp52-59.

[11] Noroozi, F., Corneanu, C. A., Kamińska, D., Sapinski, T., Escalera, S., & Anbarjafari, G. (2018). Survey on emotional body gesture recognition. IEEE transactions on affective computing, 12(2), 505-523. doi.org/10.1109/TAFFC.2018.2874986.

[12] Khalil, R. A., Jones, E., Babar, M. I., Jan, T., Zafar, M. H., & Alhusain, T. (2019). Speech Emotion Recognition Using Deep Learning Techniques: A Review. IEEE Access, 7, 117327–117345. doi:10.1109/ACCESS.2019.2936124.

[13] Ekman, P., Friesen, W. V., & Simons, R. C. (1985). Is the startle reaction an emotion?. Journal of personality and social psychology, 49(5), 1416. doi:10.1037/0022-3514.5.5.1416.

[14] Shu, L., Xie, J., Yang, M., Li, Z., Li, Z., Liao, D., Xu, X., & Yang, X. (2018). A review of emotion recognition using physiological signals. Sensors (Switzerland), 18(7). doi:10.3390/s18072074.

[15] Li, Y., Huang, J., Zhou, H., & Zhong, N. (2017). Human emotion recognition with electroencephalographic multidimensional features by hybrid deep neural networks. Applied Sciences (Switzerland), 7(10). doi:10.3390/app7101060.

[16] Setyohadi, D. B., Kusrohmaniah, S., Gunawan, S. B., Pranowo, & Prabuwono, A. S. (2018). Galvanic skin response data classification for emotion detection. International Journal of Electrical and Computer Engineering, 8(5), 4004–4014. doi:10.11591/ijece.v8i5.pp4004-4014.

[17] Hsu, Y. L., Wang, J. S., Chiang, W. C., & Hung, C. H. (2020). Automatic ECG-Based Emotion Recognition in Music Listening. IEEE Transactions on Affective Computing, 11(1), 85–99. doi:10.1109/TAFFC.2017.2781732.

[18] Song, T., Zheng, W., Lu, C., Zong, Y., Zhang, X., & Cui, Z. (2019). MPED: A multi-modal physiological emotion database for discrete emotion recognition. IEEE Access, 7(22), 12177–12191. doi:10.1109/ACCESS.2019.2895179.

[19] Miranda-Correia, J. A., Abadi, M. K., Sebe, N., & Patras, I. (2021). AMIGOS: A Dataset for Affect, Personality and Mood Research on Individuals and Groups. IEEE Transactions on Affective Computing, 12(2), 479–493. doi:10.1109/TAFFC.2018.2884461.

[20] Koelstra, S., Mühl, C., Soleymani, M., Lee, J. S., Yazdani, A., Ebrahimi, T., Pun, T., Nijholt, A., & Patras, I. (2012). DEAP: A database for emotion analysis; Using physiological signals. IEEE Transactions on Affective Computing, 3(1), 18–31. doi:10.1109/T-ACCESS.2011.15.
[21] Al-Shargie, F., Tariq, U., Alex, M., Mir, H., & Al-Nashash, H. (2019). Emotion Recognition Based on Fusion of Local Cortical Activations and Dynamic Functional Networks Connectivity: An EEG Study. IEEE Access, 7, 143550–143562. doi:10.1109/ACCESS.2019.2944008.

[22] Xu, T., Zhou, Y., Wang, Z., & Peng, Y. (2018). Learning Emotions EEG-based Recognition and Brain Activity: A Survey Study on BCI for Intelligent Tutoring System. Procedia Computer Science, 130, 376–382. doi:10.1016/j.procs.2018.04.056.

[23] Hu, X., Chen, J., Wang, F., & Zhang, D. (2019). Ten challenges for EEG-based affective computing. Brain Science Advances, 5(1), 1–20. doi:10.1177/2096598119862000.

[24] Zhang, J., Yin, Z., Chen, P., & Nichele, S. (2020). Emotion recognition using multi-modal data and machine learning techniques: A tutorial and review. Information Fusion, 59(January), 103–126. doi:10.1016/j.inffus.2020.01.011.

[25] Bhandari, N. K., & Jain, M. (2020). Emotion recognition and classification using EEG: A review. International Journal of Scientific and Technology Research, 9(2), 1827–1836.

[26] Al-Nafjan, A., Hosny, M., Al-Ohali, Y., & Al-Wabil, A. (2017). Review and classification of emotion recognition based on EEG brain-computer interface system research: A systematic review. Applied Sciences (Switzerland), 7(12). doi:10.3390/app7121239.

[27] Ladakis, I., & Chouvarda, I. (2021). Overview of biosignal analysis methods for the assessment of stress. Emerging Science Journal, 5(2), 233–244. doi:10.28991/esj-2021-01267.

[28] Made Agus Wirawan, I., Wardoyo, R., & Lelono, D. (2022). The challenges of emotion recognition methods based on electroencephalogram signals: A literature review. International Journal of Electrical and Computer Engineering, 12(2), 1508–1519. doi:10.11591/ijece.v12i2.pp1508-1519.

[29] Sarma, P., & Barma, S. (2020). Review on Stimuli Presentation for Affect Analysis Based on EEG. IEEE Access, 8, 51991–52009. doi:10.1109/ACCESS.2020.2980893.

[30] Pereira, E. T., & Martins Gomes, H. (2016). The role of data balancing for emotion classification using EEG signals. International Conference on Digital Signal Processing, DSP, 0, 555–559. doi:10.1109/ICDSP.2016.7868619.

[31] Fernández, A., García, S., Herrera, F., & Chawla, N. V. (2018). SMOTE for Learning from Imbalanced Data: Progress and Challenges, Marking the 15-year Anniversary. In Journal of Artificial Intelligence Research 61, 863–905. doi:10.1613/jair.1.11192.

[32] Nekoeimehr, I., & Lai-Yuen, S. K. (2016). Adaptive semi-unsupervised weighted oversampling (A-SUWO) for imbalanced datasets. Expert Systems with Applications, 46, 405–416. doi:10.1016/j.eswa.2015.10.031.

[33] Pradipta, G. A., Wardoyo, R., Musdolfiah, A., & Sanjaya, I. N. H. (2021). Radius-SMOTE: A New Oversampling Technique of Minority Samples Based on Radius Distance for Learning from Imbalanced Data. IEEE Access, 9, 74763–74777. doi:10.1109/ACCESS.2021.3080316.

[34] Mohammed, R., Rawashdeh, J., & Abdullah, M. (2020). Machine Learning with Oversampling and Undersampling Techniques: Overview Study and Experimental Results. 2020 11th International Conference on Information and Communication Systems, ICICS 2020, April, 243–248. doi:10.1109/ICICS49469.2020.239556.

[35] Fernández, A., García, S., Herrera, F., & Chawla, N. V. (2018). SMOTE for Learning from Imbalanced Data: Progress and Challenges, Marking the 15-year Anniversary. Journal of Artificial Intelligence Research, 61, 863–905. doi:10.1613/jair.1.11192.

[36] Ding, X. W., Liu, Z. T., Li, D. Y., He, Y., & Wu, M. (2021). Electroencephalogram Emotion Recognition Based on Dispersion Entropy Feature Extraction Using Random Over-Sampling Imbalanced Data Processing. IEEE Transactions on Cognitive and Developmental Systems, 8920(c), 1–10. doi:10.1109/TCDS.2021.3074811.

[37] Sanguanmak, Y., & Hanskunatai, A. (2016). DBSM: The combination of DBSCAN and SMOTE for imbalanced data classification. 2016 13th International Joint Conference on Computer Science and Software Engineering, JCSSE 2016, 1–5. doi:10.1109/JCSSE.2016.7748928.

[38] Sánchez, A. I., Morales, E. F., & Gonzalez, J. A. (2013). Synthetic oversampling of instances using clustering. International Journal on Artificial Intelligence Tools, 22(2), 1–21. doi:10.1142/S0218213013500085.

[39] Barua, S., Islam, M. M., Yao, X., & Murase, K. (2014). MWMOTE - Majority weighted minority oversampling technique for imbalanced data set learning. IEEE Transactions on Knowledge and Data Engineering, 26(2), 405–425. doi:10.1109/TKDE.2012.232.

[40] Bunkhumporpat, C., Sinapiromsaran, K., & Lursinsap, C. Safe-Level-SMOTE : Safe-Level-Synthetic Minority Over-Sampling Technique. Pacific-Asia Conf. Knowl. Discov. Data Min, 475–482.
Sáez, J. A., Luengo, J., Stefanowski, J., & Herrera, F. (2015). SMOTE-IPF: Addressing the noisy and borderline examples problem in imbalanced classification by a re-sampling method with filtering. Information Sciences, 291(C), 184–203. doi:10.1016/j.ins.2014.08.051.

Chen, D. W., Miao, R., Yang, W. Q., Liang, Y., Chen, H. H., Huang, L., Deng, C. J., & Han, N. (2019). A feature extraction method based on differential entropy and linear discriminant analysis for emotion recognition. Sensors (Switzerland), 19(7). doi:10.3390/s19071631.

Cheng, J., Chen, M., Li, C., Liu, Y., Song, R., Liu, A., & Chen, X. (2020). Emotion recognition from multi-channel EEG via deep forest. IEEE Journal of Biomedical and Health Informatics, 25(2), 453–464. doi.org/10.1109/JBHI.2020.2995767.

Li, J., Zhang, Z., & He, H. (2018). Research on EEG Emotional Recognition Based on LSTM. In Communications in Computer and Information Science: Vol. 1160 CCIS, 409–417. doi:10.1007/978-3-030-433-443-4_39.

Yang, Y., Wu, Q., Fu, Y., & Chen, X. (2018). Continuous convolutional neural network with 3D input for EEG-based emotion recognition. In International Conference on Neural Information Processing 433-443. Springer, Cham, Switzerland. doi.org/10.1007/978-3-030-04239-4_39.

Liu, Y., Ding, Y., Li, C., Cheng, J., Song, R., Wan, F., & Chen, X. (2020). Multi-channel EEG-based emotion recognition via a multi-level features guided capsule network. Computers in Biology and Medicine, 123(March), 103927. doi:10.1016/j.compbiomed.2020.103927.

Chao, H., Dong, L., Liu, Y., & Lu, B. (2019). Emotion recognition from multiband EEG signals using capsnet. Sensors (Switzerland), 19(9). doi:10.3390/s19092212.

Elgayar, S., A. Abdelhamid, A. E., & Fayed, Z. T. A. (2017). Emotion Detection from Text: Survey. IOSR Journal of Computer Engineering, 19(4), 30–37. doi:10.9790/0661-1904053037.

Gebhard, P. (2005). ALMA - A layered model of affect. Proceedings of the International Conference on Autonomous Agents, 177–184. doi:10.1145/1082473.1082478.

Russell, J. A. (1980). A circumplex model of affect. Journal of Personality and Social Psychology, 39(6), 1161–1178. doi:10.1037/h0077714.

Yang, Y., Wu, Q., Qiu, M., Wang, Y., & Chen, X. (2018). Emotion Recognition from Multi-Channel EEG through Parallel Convolutional Recurrent Neural Network. Proceedings of the International Joint Conference on Neural Networks, 2018(July), 1–7. doi:10.1109/IJCNN.2018.8489331.

Tyng, C. M., Amin, H. U., Saad, M. N. M., & Malik, A. S. (2017). The influences of emotion on learning and memory. Frontiers in Psychology, 8(August), 1-22. doi:10.3389/fpsyg.2017.01454.