Initial Electrochemical Activity of Magnesium Alloy AZ31 Surface Exposed to Simulated Body Fluid by Scanning Electrochemical Microscopy

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Abstract
This study applies scanning electrochemical microscopy (SECM) in feedback mode to monitor the initial activity of AZ31 magnesium alloy surface, exposed to simulated body fluid (SBF). The alloy surface suffers a degradation process since the very first moments of immersion, considered as intense uniform activity and later a localized attack was detected. The additional information provided by SEM-EDS helped to characterize the composition of sites of interest observed on the AZ31 surface. The corrosion layer contains O, C, P and Ca coming from the SBF solution, as well as the basic elements of the alloy Mg, Al, Zn and Mn. The results allowed concluding that the locally formed pits nucleated around Al-Mn intermetallic particles in contact with the Mg alloy matrix, as a consequence of chloride ions attack.

Keywords: Magnesium Alloy; AZ31; SBF; Corrosion Degradation; SEM-EDS; SECM

Introduction
Over the last years, magnesium alloys have been demonstrated to be the most promising biodegradable and resorbable materials for medical implants applications. They present physical and mechanical properties close to those of natural bone, thus avoiding the effects of stress shielding [1-6]. In addition, the released Mg ions during the implant degradation bind strongly to phosphates, which are part of physiological human solution, thus promoting bone cell attachment and tissue growth on the implants [7-11]. Many previous studies have been performed on Mg alloys, employing conventional electrochemical techniques, which only reflect the average electrochemical behavior of the entire surface. Therefore, it is necessary to assess the activity of these materials through other methods, in order to gain more information about local changes occurring at alloys surface [12,13]. Local probe techniques are a suitable option for characterizing these materials in physiological environments. Among them, the scanning electrochemical microscopy (SECM) is an advantageous tool, which allows detection of electrochemical processes in situ with high spatial and electrochemical resolution [14].

SECM in Feedback Mode: The feedback mode of SECM is the most widely used one. In this mode, a current flow through a microelectrode situated close to a substrate and immersed in an electrolytic solution having a redox mediator. Typically, the micro-disk electrode is set at a potential that allows to attain a steady state diffusion-controlled current \( i_{T,\infty} \), resulting from the electrochemical reaction of the mediator redox pair \( (O + ne^- \leftrightarrow R) \), where \( i_{T,\infty} \) becomes a function of the concentration of reactant species and its diffusion coefficient, as shown by the following equation:

\[
i_{T,\infty} = 4nFDca
\]  

where, \( n \) is the number of electrons transferred in the redox reaction, \( F \) - the Faraday constant, \( D \) - the diffusion coefficient, \( c \) - the concentration, and \( a \) is the microelectrode radius. Figure 1 illustrates the principle of operation of the feedback mode of SECM. The capabilities of SECM in this operation mode allow to monitor different systems in situ. However, only a few studies on Mg alloys have been conducted with SECM [15-24], of which not all focus on
biomedical applications. The goal of this study is to detect through SECM the initial stages of electrochemical activity on AZ31 Mg alloy surface during its exposure to buffered simulated body fluid (SBF).

Figure 1: Schematic representation of SECM feedback mode used in this work.

Experimental

Samples and Solutions Preparation: The chemical composition of AZ31 magnesium alloy (provided by Magnesium Elektron Ltd., Swinton, England) is listed in Table 1. It was fabricated in wrought condition, in the form of sheets of 2 mm thick. The alloy was cut into strips and then embedded in epoxy resin, exposing an area of 120 μm x 100 μm approximately. Before each experiment, samples were abraded with 400, 800 and 1200 grit SiC papers using ethanol as lubricant, and then polished with 0.3 μm alumina ethanolic suspension. After that, samples were sonicated in ethanol and dried in air. Finally, samples were mounted in a Teflon container, facing upwards. The simulated body fluid (SBF) was prepared using analytical grade reagents (Table 2), ultrapure deionized water (18.2 MΩ cm), and following a detailed procedure described in reference [25]. Ferrocenemethanol (FeMeOH) supplied by Across Organics (New Jersey, USA) was used as the redox mediator with a 5 mM concentration for Feedback mode of SECM test.

Table 1: Chemical composition of AZ31 Mg alloy (wt.%).

| Alloy | Al   | Zn   | Mn  | Si   | Cu   | Fe   | Ni   | Ca | Others |
|-------|------|------|-----|------|------|------|------|----|--------|
| AZ31  | 3.1  | 0.73 | 0.25| 0.02 | <0.001| 0.005| <0.001| <0.01| <0.30  |

Table 2: Reagents and their amounts for preparing 1000 mL of SBF.

| Reagent  | Amount (g) | Reagent  | Amount (g) |
|----------|------------|----------|------------|
| NaCl     | 5.403      | MgO2·6H2O| 0.311      |
| NaHCO3   | 0.740      | HEPES    | 11.928     |
| Na2CO3   | 2.046      | CaO2     | 0.293      |
| KCl      | 0.225      | Na2SO4   | 0.072      |
| K2HPO4·3H2O | 0.230   | NaOH (1.0 M) | ≈ 0.8 mL |

Instrumentation:

Scanning electrochemical microscopy (SECM) experiments were performed with an instrument built as described in references [14, 26]. Figure 2 presents an overview of the SECM setup. Optical and SEM images of the alloy surface were acquired before immersion in SBF and at the end of experiments with a BH2 model optical microscope (Olympus Co., Shinjuku, Tokyo, Japan) and a scanning electron microscope (SEM-EDS, Philips XL-30, Amsterdam, The Netherlands).

SECM experiments:

The microelectrode employed in this study was fabricated using a 7 μm diameter carbon fiber (Amoco Performance Products Inc., Chicago, IL, USA) following a procedure described in literature [27]. Figure 3 shows an optical image of the microelectrode. The electrochemical cell for SECM measurements was completed with a 0.7 mm Pt wire (Alfa Aesar, Ward Hill, MA, USA) and an Ag/AgCl/KCl reference electrode prepared using a 0.6 mm diameter Ag wire (Goodfellow Cambridge Ltd, Huntingdon, England) [28]. Positioning of the microelectrode was done with the tip set at +0.50 V in order to ensure complete diffusion-limited oxidation of ferrocene to ferrocenium. Once positioned, the tip was fixed at a constant height of 8-10 μm from the sample surface, and then the XY plane was scanned at the convenient potential for the experiment. Thus, 3D maps were obtained, where Z coordinate indicates the tip current response.

Figure 2: Schematic representation of SECM feedback mode used in this work.
Results and Discussion

Figure 4 shows the SECM maps acquired at 10 minutes, 1 hour, and 2 hours. The experiments were done with the AZ31 substrate exposed to SBF with 5.0 mM FcMeOH added as mediator. The substrate was left at its OCP and the tip performed scans at a constant height of 7 μm, with a rate of 20 μm/s and a gain of 1 nA/V. An approximate scan time of 20 minutes was required for each map. At 10 minutes of exposure (Figure 4A), the whole surface presented a relative constant value of current, reflecting a uniform electrochemical activity over the substrate. The measured current activity (iT) increased after 1 hour of exposure (Figure 4B) and the uniform behavior on the surface continued. An increase in the electron transfer rate (current value) could be related to changes in the alloy surface, related to higher corrosion rate even in the presence of corrosion layer. After 2 hours of exposure (Figure 4C), the surface presented a noticeable localized corrosion in some most active sites, where the current values increased. The above is usually attributed to nucleation of pits, as a consequence of more pronounced chloride ions attack. The provided optical images reveal an evidence of the changes that AZ31 substrate suffered at the end of the exposure to SBF.

Figure 5 presents SEM images of the bare AZ31 surface (A) and after 2 hours of its exposure to SBF (B). The matrix (Figure 5-site 1) presents the basic alloying elements, corresponding to AZ31 (Figure 6 site 1). It can be observed that on AZ31 surface there are particles (in white color) (Figure 5A site 2), which EDS analysis (Figure 6-site 2) indicates that their composition could be attributed to the intermetallic Al-Mn secondary phase [29-33]. It is considered that these particles have less negative corrosion potentials than the Mg-matrix (-1.52 to -1.25 V vs SCE), so they could act as local cathodes, according to study of several magnesium alloys in 5% NaCl solution [34-37]. Thereby, pit nucleation could take place around areas where Mg-matrix is in contact with those particles.
locally distributed cathodes on the AZ31 surface. It could be also seen that the formed corrosion layer is cracked (Figure 5B). The SEM observed pits nucleation correlate well with the localized surface activity detected in the map of SECM (Figure 4C) after the exposure in SBF.

![Figure 5](image1.png)

**Figure 5**: SEM images of AZ31 surface: (A) before and (B) after its exposure to SBF for 2 hours.

EDS analysis (Figure 6-site 3) of the corrosion layer of site 3 (Figure 5B-site 3) indicates that it contains C, O, P and Ca elements coming from the SBF solution, besides the basic elements of the alloy (Mg, Al, Zn). The pits (Figure 5-site 4) present Mn as an additional element (Figure 5-site 4), as a part of the local cathodes of Al-Mn, where the localized corrosion takes place. The main reported corrosion products for AZ31 in SBF are Mg(OH)$_2$ and Ca$_{10}$(PO$_4$)$_6$(OH)$_2$ [38-42].

![Figure 6](image2.png)

**Figure 6**: EDS elemental analysis of sites marked in SEM images (Figure 5).

**Conclusion**

Correlating SECM and SEM-EDS obtained results, it can be suggested that the initial behavior of AZ31 magnesium alloy exposed to buffered simulated body fluid (SBF) is as follows:

a) Since the very first moments of immersion, the alloy surface undergoes intense electrochemical activity related to a fast degradation and formation of a corrosion layer.

b) Such layer is susceptible to chloride ions penetration which accelerates the localized corrosion.

c) The pits nucleation is promoted by the presence of microgalvanic pairs of Al-Mn cathodic particles and the anodes of the Mg alloy matrix.

**References**

1. Witte F (2005) *In vivo* corrosion of four magnesium alloys and the associated bone response. Biomaterials 26(17): 3557-3563.

2. Staiger MP (2006) Magnesium and its alloys as orthopedic biomaterials: a review. Biomaterials 27(9): 1728-1734.

3. Razavi M, Fathi MH, Meratian M (2010) Microstructure, mechanical properties and bio-corrosion evaluation of biodegradable AZ91-FA nanocomposites for biomedical applications. Materials Science and Engineering: A 527(26): 6938-6944.

4. Feng A, Han Y (2010) The microstructure, mechanical and corrosion properties of calcium polyphosphate reinforced ZK60A magnesium alloy composites. Journal of Alloys and Compounds 504(2): 585-593.

5. Seal CK, Vince K, Hodgson MA (2009) Biodegradable surgical implants based on magnesium alloys-A review of current research. IOP Conference Series: Materials Science and Engineering 4: 012011.
