Intrasubject subcortical quantitative referencing to boost MRI sensitivity to Parkinson’s disease

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A B S T R A C T

Several postmortem studies have shown iron accumulation in the substantia nigra of Parkinson’s disease patients. Iron concentration can be estimated via MRI-R₂₀ mapping. To assess the changes in R₂₀ occurring in Parkinson’s disease patients compared to controls, a multicentre transversal study was carried out on a large cohort of Parkinson’s disease patients (n = 163) with matched controls (n = 82). In this study, 44 patients and 11 controls were removed due to motion artefacts, 21 patient and 6 controls to preserve matching. Thus, 98 patients and 65 age and sex-matched healthy subjects were selected with enough image quality.

The study was conducted on patients with early to late stage Parkinson’s disease. The images were acquired at 3Tesla in 12 clinical centres. R₂₀ values were measured in subcortical regions of interest (substantia nigra, red nucleus, striatum, globus pallidus externus and globus pallidus internus) contralateral (dominant side) and ipsilateral (non dominant side) to the most clinically affected hemisphere.

As the observed inter-subject R₂₀ variability was significantly higher than the disease effect, an original strategy (intrasubject subcortical quantitative referencing, ISQR) was developed using the measurement of R₂₀ in the red nucleus as an intra-subject reference.

R₂₀ values significantly increased in Parkinson’s disease patients when compared with controls; in the substantia nigra (SN) in the dominant side (D) and in the non dominant side (ND), respectively (P_{SN,D} and P_{SN,ND} < 0.0001). After stratification into four subgroups according to the disease duration, no significant R₂₀ difference was found in all regions of interest when comparing Parkinson’s disease subgroups.

By applying our ISQR strategy, R₂₀\_ISQR values significantly increased in the substantia nigra (P_{SN,D} and P_{SN,ND} < 0.0001) when comparing all Parkinson’s disease patients to controls.

R₂₀\_ISQR values in the substantia nigra significantly increased with the disease duration (P_{SN,D} = 0.01; P_{SN,ND} = 0.03) as well as the severity of the disease (Hoehn & Yahr scale <2 and ≥ 2, P_{SN,D} = 0.02). Additionally, correlations between R₂₀\_ISQR and clinical features, mainly related to the severity of the disease, were found.

Our results support the use of ISQR to reduce variations not directly related to Parkinson’s disease, supporting the concept that ISQR strategy is useful for the evaluation of Parkinson’s disease.

1. Introduction

Post mortem histological analysis (Dexter et al., 1989; Riederer et al., 1989), showed the concentration of iron increasing from 30 to 100 % in the substantia nigra of Parkinson’s disease patients compared to controls. However, results are controversial in other basal ganglia structures (Wei and Wang, 2016). At the pathophysiological level, the overload of iron storage in the substantia nigra exaggerates oxidative stress, accelerates aggregation of alpha-synuclein (Wolozin and Golts, 2002) and may lead to cell damage.

Magnetic resonance imaging (MRI) is a powerful tool used to detect iron deposits in the brain as its paramagnetism induces magnetic field inhomogeneities that accelerate relaxation rates (Tosk et al., 1992; Brooks et al., 1989; Schenck, 1995). In vivo (Gelman et al., 1999) and post mortem (Langkammer et al., 2010) studies converged in showing that both R₂ and R₂₀ transverse relaxation rates are influenced by the presence of iron in the brain. R₂ and R₂₀ are both linearly and positively correlated with iron concentration, with roughly similar respective slopes. Because R₂₀ is made up of the sum of these two irreversible (R₂) and reversible (R₂₀) components, R₂₀ is thus more sensitive to iron content. In addition, R₂₀ can be easily mapped in the brain by using magnitude of gradient recalled echo images at multiple echo times (Chavhan et al., 2009).

R₂₀ variations due to Parkinson’s disease have been extensively studied in vivo. With rare exceptions (Liu et al., 2019; Reimão et al., 2015), most of the studies have demonstrated higher R₂₀ in the substantia nigra of Parkinson’s disease patients (Barbosa et al., 2015; Baudrexel et al., 2010; Du et al., 2018; Du et al., 2011; Graham et al., 2000; Guan et al., 2017; Hopes et al., 2016; Langkammer et al., 2016; Langley et al., 2017; Lewis et al., 2013; Martin and Gee, 2008; Péran et al., 2010; Ulla et al., 2013; Wallis et al., 2008). In basal ganglia (caudate nucleus, putamen, globus pallidus), recent studies found no change of R₂₀ (Barbosa et al., 2015; Baudrexel et al., 2010; Guan et al., 2017; Hopes et al., 2016; Langkammer et al., 2016; Martin and Gee, 2008; Péran et al., 2010). If elevated iron levels could lead to dopaminergic neuron denervation in the substantia nigra of Parkinson’s disease patients, links between R₂₀ values and clinical characteristics of patients with Parkinson’s disease such as disease duration and severity should be observed. In fact, although longitudinal studies have confirmed that variation in R₂₀ may capture Parkinson’s disease-related progression in the substantia nigra (Du et al., 2018; Hopes et al., 2016; Ulla et al., 2013), others failed to detect a longitudinal change (Arribar et al., 2019; Wieler et al., 2015) or showed that rather than correlating with disease duration, the rate of change was associated with individual characteristics, such as cognitive decline and age in later stages of Parkinson’s disease (Rossi et al., 2014).

Looking at the data in the literature, R₂₀ is not considered to be very sensitive as an indicator of disease progression.

The strategy implemented by these studies was the search for a mean group effect which implicitly neglects the inter-subject variability by treating it as noise. However, when reported, the between-subject standard deviation of R₂₀ in substantia nigra was between 15 and 20 %, in patients as well as controls. Such high variability of R₂₀ could limit the use of this parameter as a surrogate biomarker in order to track the progression of Parkinson’s disease.

Several factors can explain such inter-subject variability; (i) the biological heterogeneity of parkinsonian patients, e.g. the large range of age (47 to 72 years) and duration of disease (1–13 years) (Pyatigorskaya et al., 2020), (ii) positioning errors when defining the substantia nigra region which differ according to the segmentation techniques used (e.g. manual or automatic), (iii) differences in measurement conditions.

1 Collaborators in the R² study are listed in the Appendix.
which cannot be strictly standardized from one subject to another, e.g. orientation of the head in the coil, (iv) the structural factors contributing to the subtle magnetic properties of the brain which thus may change $R_2^*$ of the substantia nigra independently from the disease, e.g. the surrounding myelin (Duyn, 2017).

The role of this cross-sectional study is to clarify how much $R_2^*$ is changing as a function of the disease stage while tackling several of the issues that arise due to inter-subject variability. First, it was designed to measure $R_2^*$ values in subcortical regions of interest (substantia nigra, red nucleus, striatum, globus pallidus externus and globus pallidus internus) contralateral (dominant side) and ipsilateral (non dominant side) to the most clinically affected hemibody, in four groups of patients from early to late stages of the disease and matched controls. Clinical data assessing motor and non-motor signs was assessed to measure the severity of the disease. In addition, a new intra-subject referencing technique was introduced in order to isolate the variation of $R_2^*$ associated with Parkinson’s disease from other sources of $R_2^*$ variance.

2. Materials and methods

2.1. Study subjects

This study was an ancillary part of the IPD-R2 study which is an ongoing multicentre prospective study of Parkinson’s disease patients assessing the amount of iron in the brain by MRI. Patients were recruited between August 2015 – June 2019 by 12 French University hospitals of the French national NS-Park/FCRIN network (https://www.parkinson.network/).

The protocol was approved by the research ethical committee (Comité de Protection des Personnes, AU1135, France). All participants gave written informed consent. The study was registered on the clinicaltrials.gov website (Ref. Clinical Trial = NCT02816645). Inclusion criteria was diagnosis of Parkinson’s disease according to MDS clinical criteria for Parkinson’s disease (Postuma et al., 2015). Exclusion criteria were severe cognitive impairment (Montreal Cognitive Assessment (MoCA) < 24) (Nasreddine et al., 2005) and atypical parkinsonism. Clinical data were collected at baseline, and one year later. MRI was performed at the baseline visit and then one year later to evaluate variations of volume structures, diffusion parameters, and iron content. Here, only clinical and $R_2^*$ measurements from MRI data obtained at baseline were used.

2.2. Study design and clinical scores

Patients were selected according to duration of disease (Group1 (G1) < 5 years, Group2 (G2) ≥ 5 and < 10 years, Group3 (G3) ≥ 10 and < 15 years and Group4 (G4) ≥ 15 years) with the aim of recruiting 40 patients per subgroup. Control subjects were matched for each subgroup according to age (±5 years) and sex.

Clinical assessments at baseline included collection of demographic data, medical and treatment history. Parkinsonism evaluation was assessed using the Movement Disorder Society-Unified Parkinson’s Disease Rating Scale (MDS-UPDRS) parts I-IV (Goetz et al., 2008) which assesses non-motor and motor performances of daily living (MDS-UPDRS I, II), motor examination (MDS-UPDRS III) and motor complications (MDS-UPDRS IV), the Hoehn & Yahr (H&Y) scale (Hoehn and Yahr, 1998), the Schwab & Englund (S&E) scale (Schwab, 1960) and the Freezing of Gait Questionnaire (FOG-Q) (Gilladi et al., 2009). To determine the most affected hemibody, the sum of the following MDS-UPDRS III items were calculated for the left and right hemibody: rigidity, finger tapping, hand movements; pronation-supination movements of hands; toe tapping; leg agility, postural and kinetic tremor of the hands; rest tremor amplitude for upper and lower limbs. The body side with the higher score for these items was considered as the dominant side. In addition, a neuropsychological assessment was performed, using a MoCA for global efficiency, the Lille Apathy Rating Scale (LARS) (Sockeel et al., 2006), the Hamilton Rating Scale for Depression (HAM-D) (Hedlund and Vieweg, 1979) and the Hamilton Rating Scale for Anxiety (HAM-A) (Hamilton, 1959). Regarding psycho-behavioral symptoms, the French version of Ardouin scale of Behavior in Parkinson’s Disease (ASBPD) was used to assess hypo and hyperdopaminergic disorders, non-motor fluctuations and impulse-control disorders (ICD) (compulsive eating, hobbyism, punding, compulsive shopping, pathological gambling, hypersexuality, dopaminergic addiction) (Rieu et al., 2015). Finally, self-questionnaires were completed, including the Epworth Sleepiness Scale (ESS) (Johns, 1991), the assessment of Autonomic Dysfunction in Parkinson’s Disease (SCOPA-AUT) (Visser et al., 2004) and Non-Motor Symptom Assessment Scale for Parkinson’s Disease (NMSS) (Chaudhuri et al., 2006). The Levodopa Equivalent Daily Dose (LED) was provided for each patient taking into account levodopa treatments, dopamine agonists, and other antiparkinsonian drugs such as MAO-B inhibitors, COMT inhibitors and amantadine (Tomlinson et al., 2010). Regarding healthy control subjects, the LARS, HAM-A and HAM-D were performed in addition to the MoCA. A maximum of ± 3 months was allowed between clinical evaluations and MRI acquisition.

2.3. MRI data acquisition

MRI was performed at 3T by 12 French clinical centres with different magnetic resonance imaging scanners. Sixty-six patients with Parkinson’s disease and 32 healthy controls were scanned with a General Electric MRI scanner (GE Healthcare, Waukesha, WI, USA), 35 Parkinson’s disease patients and 14 healthy controls with a Philips MRI scanner (Philips, Best, Netherlands), 62 Parkinson’s disease patients and 36 healthy controls subjects with a Siemens MRI scanner (Siemens, Erlangen, Germany) (see Supplementary Information Table, Table 1).

The implementation of the MRI protocol at the 12 centres was carried out in collaboration with the CATI platform (Centre for Image Acquisition and Processing, Neurospin, CEA, Saclay, France, https://ca ti-neuroimaging.com). All MRI systems used identical three-dimensional (3D) multiple GRE sequences with matching parameters, in order to limit inter-site variability. The protocol was designed to obtain images in less than ten minutes in order to reduce the effect of head movement (Gay et al., 2016). Datasets were acquired on the NIST test-object (Russek et al., 2012) to confirm the between-centre consistency of the $R_2^*$ measurement. Protocol consistency monitoring and quality control was ensured by CATI for the duration of the study.

All subjects were equipped with a multichannel receive-only array head coil and were immobilized by foam pads during acquisition to reduce involuntary head movements. Disposable ear plugs were also used to reduce acoustic noise. The sequence parameters were as follows: field of view $256 \times 256 \times 160$ mm$^3$, leading to a voxel volume of $1 \times 1 \times 1$ mm$^3$; 6 equidistant echo times (TE = 4.28, 9.54, 14.79, 20.05, 25.31, 30.56 ms). The duration of the 3D multiple GRE sequence was about 10 min.

Acquired datasets were evaluated regarding their reliability for further analyses and divided into three categories: reject, borderline and OK. The quality control for 3D multi GRE sequences was based on a systematic procedure, to try to minimise subjective assessment. Relative uncertainty maps were computed together with $R_2^*$ single exponential maps. Mean values were computed in regions coregistered from the AAL atlas (lentiform nuclei and thalamus) to give a first estimate of measurement reliability, by comparing the values to thresholds previously estimated on another database. However, local values only give information on the underlying area. These values were thus confirmed by a systematic overall visual evaluation on the first, third and fifth echoes, together with the $R_2^*$ and uncertainty maps displayed with predefined ranges and colormaps, to rate specific artefacts according to a three point grade, mainly wrinkles due to motion, blur due to motion, artefacts localised in the area of interest, artefacts due to eye motion and artefacts due to susceptibility (0 meaning no visible artefact, 1...
indicating an artefact but the underlying structure is still well defined and 2 indicating that the underlying borders are no longer correctly defined because of the artefact). A global qualitative index and a final decision are then inferred from these items, thus giving a more objective basis to this rating.

Data of lower quality were excluded from analysis (reject category).

2.4. MRI data processing and analysis

2.4.1. \( R_2^* \) mapping

The six magnitude GRE images for each participant were spatially normalized using standard SPM12 procedures (Statistical Parametric Mapping, Wellcome Department of Cognitive Neurology, London, UK). To correct for any between-echo misregistration, the images were linearly registered to the first TE image using the SPM tool REALIGN in order to estimate and apply a rigid-body affine transformation with 6 degrees of freedom and cubic spline interpolation. Then, to segment into grey matter, white matter and CSF probability maps, the first echo of each subject image was used, utilizing the “new segment” approach (Ashburner and Friston, 2005). Lastly, the DARTEL pipeline was used for spatial normalization in which a study specific group template is created using an iterative process (Ashburner, 2007). The obtained subject-specific deformation fields were then applied to normalize the six TE images to the standard MNI space. This preprocessing step was only based on the multi-TE acquisitions and did not require further anatomical MRI, which reduced the risk of residual misregistration. Because the DARTEL pipeline is inherently a group-level procedure, all subjects belonging to a given group were spatially-normalized together. Hence, the DARTEL was applied to the four Parkinson’s disease subgroups and the four control groups separately.

For \( R_2^* \) mapping, these registered and spatially-normalized GRE images were non-linearly fitted voxel wise in the least-squares sense with a mono-exponential model as a function of TEs using an in-house MATLAB script (LSQNONLIN function). Hence the \( R_2^* \) maps were de facto obtained by the MNI reference space.

2.4.2. Regions of interest

10287005360670000Regions of interest were defined according to the freely available ATAG probabilistic atlas (Keuken, 2014; Keuken and Bu, 2015). Five basal ganglia structures were selected: the substantia nigra, the red nucleus, the striatum, the globus pallidus externus and the globus pallidus internus. The degrees of membership were limited to 0.70 so as to fit to the structures and in particular to the SN (cf. Supplementary Fig. 1). \( R_2^* \) values were measured in the dominant and non-dominant sides in each brain structure. Grey matter and white matter regions were obtained from the previous segmentation step (new segment) using thresholding at \( P = 0.95 \).

To validate our automatic segmentation, the substantia nigra was also contoured manually on images of thirty control subjects. The manual contouring was performed by an expert neurologist in the field (F.D.). The manual segmentation was based on a single T2*-weighted image (GRE at TE = 25.3 ms) according to the previously described methods (Eapen et al., 2011) and a MRI atlas of the mesencephalon (Duvernoy, 1995) using ITK-SNAP (www.itksnap.org) (Yushkevich et al., 2006). A significant \( R_2^* \) correlation between automatic and manual contouring in controls was shown (substantia nigra = SN; \( r_{SN,D} = 0.73 \), \( r_{SN,ND} = 0.76 \) and both \( P < 0.01 \)).

2.4.3. Intrasubject subcortical quantitative referencing (ISQR)

In our study, the \( R_2^* \) inter-subject variability (i.e. the relative standard deviation of \( R_2^* \) within the considered group) obtained both in Parkinson’s disease patients and controls was substantial, between 10 and 20 %. This variability was mostly independent of the disease (see results and the discussion). In order to remove this non-specific variability (i.e. between-subject \( R_2^* \) variation independent of the disease), the red nucleus was chosen as a reference structure for the following four reasons: (i) the red nucleus is not directly involved in the pathophysiology of Parkinson’s disease (ii) no significant difference in \( R_2^* \) was found between patients and control subjects in this region (Table 2) (iii) the values of \( R_2^* \) in the red nucleus were close to those observed in the basal ganglia and specifically in the substantia nigra (Table 2) and (iv) \( R_2^* \) in the red nucleus and in the substantia nigra were correlated for control subjects (red nucleus = RN; \( R_{SN,D} = 0.56 \), \( P_{SN,D} = 0.001 \), \( R_{SN,ND} = 0.49 \), \( P_{SN,ND} = 0.001 \)). Therefore, in addition to considering the raw value of \( R_2^* \) averaged in the different anatomical regions, we also considered the difference between this value and the one measured on the red nucleus, i.e.

\[
R_{ISQR,k}(\text{region of interest, subject}) = R_{2*}(\text{region of interest, subject}) - R_{2*}(\text{red nucleus, subject})
\]

The rationale of ISQR considers ferritin, which is mainly located within the subcortical nuclei, and neuromelanin, which is more specific of dopaminergic neurons in the SN, are two independent compartments. These field creating objects thus act on the T2 relaxation as two multi-plicative mono-exponential decays which give rise to a total apparent decay in which the relaxation rates of the two compartments add. Following these assumptions, subtracting the \( R_2^* \) value of the red nucleus is a natural operation for removing the influence of individual variation independent of the disease.

2.5. Statistical analysis

Sample size was calculated according to (i) Cohen’s recommendations (Cohen, 1988) which define effect-size bounds as small (ES: 0.2), medium (ES: 0.5) and large (ES: 0.8, “grossly perceptible and therefore large”) and (ii) to the work of Marek et al. (Marek et al., 2011), in which for every-two participants, at least one control participant was included.

Continuous data were expressed as mean and standard-deviation or median and interquartile range, according to statistical distribution. The assumption of normality was assessed using the Shapiro-Wilk test. The comparisons between groups (i.e. between disease duration sub-groups) were performed using linear mixed model taking into account centre and machine effects (as random-effects), and when appropriate, pairing effect for patient vs control subject comparisons. The normality of residuals from these models was studied using the Shapiro-Wilk test. When necessary, a logarithmic transformation was applied to achieve the normality of dependent outcomes. The results were expressed using Hedge’s effects-size and were interpreted according to the aforementioned Cohen’s rules of thumb. To take into account our multiple comparison study, a Sidak’s type 1 error correction was applied. Then, multivariate analyses have been performed using adjustment on covariates fixed according to the univariate results and to the clinical relevance: HY, treatment, MDS-UPDRS part IV and quality of images. A particular attention was paid on multicollinearity of covariates. Effect-sizes were then compared according to disease duration by the analyze of interaction between PD and healthy subjects in multivariate analyses. The relationships between quantitative variables were
analyzed using correlation coefficients (Pearson or Spearman, according to the statistical distribution). The results were represented using a color heatmap. A Sidak’s type I error correction was applied to take into account multiple comparisons.

Finally, discriminant factorial analysis was performed (i) to illustrate the relationship between clinical characteristics and \( R^2 \) parameters using principal component analysis and then (ii) to highlight associations between \( R^2 \) parameters and disease duration with discriminant analysis. These statistical methods were useful for analyzing assets as elements of quantitative variables in order to uncover the underlying relationships and structures of the variables measured (latent constructs) and to aggregate subjects into clusters such that each cluster represents a topic (i.e. disease duration).

Analyses were performed with Stata 15.0 (StataCorp, College Station, US) and software R (package ade4) for factorial analyses. The tests were two-sided, with a type I error set at 5 %.

3. Results

3.1. Demographic information

One hundred and sixty-three patients with Parkinson’s disease and 82 age and sex-matched controls were recruited at baseline. Forty-four patients and 11 controls were excluded from the analysis after rejection of the 3D multiple GRE sequence during the CATI quality control procedure due to movements or the presence of artifacts, i.e. 27 % of patients and 14 % of controls. The exclusion of the other subjects (21 patients and 6 controls) is related to our desire to keep the matching between patients and controls. Thus, 98 Parkinson’s disease patients (60 males and 38 females) and 65 age and sex-matched healthy subjects (35 males and 30 females) were selected with enough image quality, i.e. low noise and fewer artifacts (Fig. 1).

Table 1 summarizes the demographic and clinical characteristics of the subjects. Compared to controls, Parkinson’s disease patients had significantly higher HAM-D scores \((P = 0.02)\) and LARS-scores \((P = 0.001)\). Moreover, a significant difference was observed between the Parkinson’s disease subgroups according to disease duration and MDS-UPDRS IV \((P = 0.001)\), FOG-Q \((P = 0.001)\), H&Y ON \((P = 0.02)\) and LEDD \((P = 0.001)\). A significant difference was observed also when comparing MDS-UPDRS III ON_D. vs MDS-UPDRS III ON_ND in all Parkinson’s disease patients and in each Parkinson’s disease sub-groups \((p < 0.001)\).
### 3.2. Machine/center effects

Our current study was carried out by 12 clinical centres, with a variety of MRI scanners (General Electric, Philips, and Siemens). No difference in $R_2^*$ values in the SN between the machines (for healthy controls; PSND and PSNND = 0.13 and for PD patients; PSND = 0.62 and PSNND = 0.35) and the centres (for healthy controls; PSND and PSNND = 0.23 and for PD patients; PSND = 0.78 and PSNND = 0.88) were found in this study (see Supplementary Information Table, Table 1 and Table 2).

The acquisition parameters of the 3D Multiple-GRE sequence for each scanner used in this study were shown in Supplementary Information Table, Table 5.

### 3.3. $R_2^*$ and $R_2^{*SDOR}$ results

#### 3.3.1. Parkinson’s disease patients versus controls

All $R_2^*$ values and $R_2^{*SDOR}$ values are displayed in Table 2. $R_2^*$ values and $R_2^{*SDOR}$ values significantly increased in Parkinson’s disease patients when compared with controls; in the substantia nigra in the dominant side and in the non-dominant side respectively ($P_{SDO,D}$ and $P_{SN,ND} < 0.0001$; on both measures). In addition, $R_2^*$ values significantly increased in grey matter (grey matter = GM; $P_{GM} = 0.03$) and in white matter (white matter = WM; $P_{WM} = 0.03$).

#### 3.3.2. Parkinson’s disease patients according to disease duration

All the results of $R_2^*$ values between the subgroups are summarized in Table 2. There was no significant difference for raw $R_2^*$ values between the subgroups in all regions of interest. $R_2^{*SDOR}$ values in the substantia nigra increased with the disease duration ($P_{SDO,D} = 0.01$; $P_{SN,ND} = 0.03$). Fig. 2 presents the effect sizes between Parkinson’s disease subgroups in the dominant side and non-dominant side in the substantia nigra using the $R_2^{*SDOR}$ values. The analyses were adjusted to HY, treatment, MDS-UPDRS part IV and quality of images. A significant difference in the effect size of $R_2^{*SDOR}$ values between Parkinson’s disease subgroups ($P < 0.05$), as well as when comparing PD patients-G3 vs PD patients-G1 ($P_{SDO,D} = 0.03$, $P_{SN,ND} = 0.01$) and when comparing PD patients-G4 vs PD patients-G1 ($P_{SDO,D} < 0.001$, $P_{SN,ND} = 0.01$) was showed.

#### 3.3.3. Parkinson’s disease patients according to disease severity

During the course of the study, two new sub-groups were created based on the severity of the disease (H&Y < 2, n = 28 and H&Y ≥ 2, n = 70). Values are listed in Table 2. For all regions, no difference in $R_2^*$...
Table 2

| R2 (raw data) | All PD patients | R2_inSBOR | Disease duration | R2_inSBOR | Disease severity |
|---------------|-----------------|-----------|------------------|-----------|-----------------|
| Number of subjects | 98 | 65 | 31 | 26 | 26 | 15 | 28 | 70 |

| SN_D | 39.23 ± 5.85 | 34.94 ± 3.83 | 39.48 ± 5.24 | 38.87 ± 7.11 | 41.96 ± 5.65 | 38.54 ± 4.89 | 39.51 ± 6.21 | <0.0001 | 0.16; 0.75 |
| SN_ND | 38.88 ± 5.38 | 34.94 ± 4.86 | 37.29 ± 3.59 | 39.59 ± 5.63 | 39.63 ± 7.2 | 40.09 ± 5.18 | 38.28 ± 4.8 | 39.12 ± 5.77 | <0.0001 | 0.37; 0.05 |
| RN_D | 33.42 ± 4.39 | 34.48 ± 4.3 | 33.35 ± 4.82 | 34.67 ± 7.1 | 32.75 ± 5.05 | 32.33 ± 2.46 | 34.75 ± 4.03 | 32.87 ± 4.44 | 0.14 | 0.14; 0.06 |
| RN_ND | 33.51 ± 4.59 | 34.48 ± 3.83 | 33.84 ± 3.99 | 34.62 ± 5.31 | 32.33 ± 2.9 | 32.7 ± 1.2 | 34.13 ± 4.25 | 33.26 ± 4.72 | 0.19 | 0.32; 0.42 |
| GPi_D | 28.64 ± 5.01 | 29.87 ± 4.72 | 29.57 ± 4.39 | 27.34 ± 4.15 | 28.67 ± 6.43 | 28.81 ± 4.99 | 28.39 ± 4.63 | 28.75 ± 5.19 | 0.1 | 0.56; 0.79 |
| GPi_ND | 28.6 ± 4.44 | 29.87 ± 4.72 | 29.57 ± 4.39 | 27.34 ± 4.15 | 28.67 ± 6.43 | 28.81 ± 4.99 | 28.39 ± 4.63 | 28.75 ± 5.19 | 0.1 | 0.56; 0.79 |
| GPe_D | 34.44 ± 4.22 | 35.3 ± 4.44 | 35.21 ± 3.44 | 34.32 ± 3.45 | 34.08 ± 3.51 | 33.33 ± 4.78 | 34.82 ± 3.98 | 34.29 ± 4.34 | 0.2 | 0.75; 0.73 |
| GPe_ND | 34.76 ± 4.44 | 35.3 ± 4.44 | 34.89 ± 4.32 | 34.33 ± 3.33 | 35.25 ± 4.36 | 34.59 ± 4.63 | 35.18 ± 4.46 | 34.6 ± 4.37 | 0.44 | 0.85; 0.88 |
| STR_D | 27.28 ± 3.06 | 28.46 ± 3.21 | 27.4 ± 3.21 | 27.4 ± 3.21 | 27.0 ± 3.21 | 26.7 ± 3.21 | 28.26 ± 2.98 | 28.7 ± 3.27 | 0.06 | 0.61; 0.13 |
| STR_ND | 27.28 ± 3.06 | 28.46 ± 3.21 | 27.4 ± 3.21 | 27.4 ± 3.21 | 27.0 ± 3.21 | 26.7 ± 3.21 | 28.26 ± 2.98 | 28.7 ± 3.27 | 0.06 | 0.61; 0.13 |
| GM | 20.1 ± 2.1 | 19.7 ± 1.3 | 19.7 ± 1.3 | 19.7 ± 1.3 | 19.7 ± 1.3 | 19.7 ± 1.3 | 20.1 ± 2.1 | 20.1 ± 2.1 | 0.03 | 0.03 |
| WM | 20.8 ± 0.8 | 20.5 ± 0.8 | 20.5 ± 0.8 | 20.5 ± 0.8 | 20.5 ± 0.8 | 20.5 ± 0.8 | 20.8 ± 0.8 | 20.8 ± 0.8 | 0.03 | 0.03 |

Values are expressed as Mean ± standard deviation; PD = Parkinson’s disease; na = not applicable; SN_D = substantia nigra_dominant; SN_ND = substantia nigra_non dominant; RN_D = red nucleus_dominant; RN_ND = red nucleus_non dominant; GPe = globus pallidus externus_dominant; GPe_ND = globus pallidus externus_non dominant; GPi = globus pallidus internus_dominant; GPi_ND = globus pallidus internus_non dominant; STR = striatum_dominant; STR_ND = striatum_non dominant; G2 = grey matter; WM = white matter. G1: Group 1 < 5 years; G2: Group 2 > 5 and ≤ 10 years; G3: Group 3 > 10 and ≤ 15 years; G4: Group 4 > 15 years.

* : statistical significance between patients and healthy controls.

† : statistical significance between the PD subgroups according to disease duration.

‡ : statistical significance between the PD subgroups according to disease severity.

Values was found between these two subgroups. However, there was a significant increase in R2_inSBOR values in patients with H&Y ≥ 2 compared to H&Y < 2 in the substantia nigra in the dominant side of the disease (P<0.01).

3.3.4. Correlation results of R2 / R2_inSBOR

Positive correlations were found between the R2 values and asBDSP1&II in -GPi (r_GPi_D = 0.23, r_GPi_ND = 0.05) and in -GPe (r_GPe_D = 0.04; r_GPe_ND = 0.03) were found (Fig. 3A).
As described previously, a moderate correlation between values of patients in all regions of interest (without clinical data) were values of the patients and the clinical parameters included in this study.

-0.3, values between Parkinson...

4. Discussion

In this multicentre study, the changes in $R_2^*$ relaxation rate, which reflects iron concentration, was studied as a function of the duration and severity of Parkinson’s disease, while taking into account the inter-subject variability of the $R_2^*$ parameter. We first considered the average $R_2^*$ within several basal ganglia regions and then developed an original approach using an internal reference in order to highlight the variation in $R_2^*$ linked to Parkinson’s disease compared to other sources of $R_2^*$ variance.

Our ISQR approach allowed us to obtain a significant difference when comparing the different groups of patients to their controls. When analyses were controlled by H&Y, treatment, MDS-UPDRS part IV and quality as covariables in multivariate analyses in addition to centre and machine as random-effects, the results were not changed. In addition, ISQR can be used to show a progressive increase of the magnitude effect of the $R_2^*$ parameter in the substantia nigra in parkinsonian patients according to the disease duration, taking into account the paired effect, the centre and machine effects and image quality. Finally, correlations are also observed between the $R_2^*$ of several regions of interest with the clinical characteristics of Parkinson’s disease (age, duration of disease, severity, motor and non-motor symptoms). This is in line with current concepts recognizing that dysfunctions within the basal ganglia induce cognitive and behavioral deficits in addition to the motor symptoms of Parkinson’s disease (Tremblay et al., 2015). These results enable to consider the use of this parameter as a potential marker of the progression of the disease.

4.1. Comparison of the results with previous studies

In our study, a significant difference was shown for $R_2^*$ values between patients with Parkinson’s disease and control subjects in the substantia nigra, which was consistent with the results of most previous studies (Graham et al., 2000; Martin and Goo, 2008; Péran et al., 2010; Du et al., 2012; Ulla et al., 2013; Wieler et al., 2015; Pyatigorskaya et al., 2015) except those by (Reimão et al., 2015).

In addition and especially without applying the ISQR approach, no effect of disease duration and severity assessed with H&Y scale on $R_2^*$ parameters were shown in our study. These results are in line with previous $R_2^*$ - based cross-sectional studies (Gorell et al., 1995; Graham et al., 2000; Martin and Goo, 2008; Péran et al., 2010; Du et al., 2011; Barbossa et al., 2015; Cheng et al., 2020) which also did not find a significant correlation between increased susceptibility values in the substantia nigra and disease duration in patients with Parkinson’s disease, but the elevated...
R² values in the substantia nigra were not correlated with clinical features. Langkammer et al. (Langkammer et al., 2016) demonstrated that the substantia nigra susceptibility values were correlated with H&Y scales but were not correlated with disease duration in patients with Parkinson’s disease. Finally, if longitudinal studies have confirmed that variation in R² may capture Parkinson’s disease-related progression in the substantia nigra (Du et al., 2018; Hopes et al., 2016; Ulla et al., 2013), others failed to detect a longitudinal change (Arribar et al., 2019; Wieler et al., 2015).

The previous attempts at finding correlations between R² and severity or disease duration were somewhat contradictory. This may be explained by different sources of variability that reduce the sensitivity and accuracy of R² mapping. Variability can be due to the heterogeneity of the studied populations and also to instrumental variability (i.e. noise). Moreover, part of the inter-subject variability may be unrelated to disease. This is the main reason that led to develop the ISQR strategy with the aim of reducing large inter-subject variability (10–20 %) not related to disease in the regions of interest.

4.2. ISQR strategy interest

ISQR is introduced for the first time in this study. It is based on the finding that a significant part of the inter-subject variability of R² in most subcortical regions is not related to Parkinson’s disease. By removing most of this variability using ISQR, our results allowed us to estimate the effect size due to Parkinson’s disease as function of the duration and severity of the disease. It shows that this effect size is comparable to the unexplained variance. For example, when comparing patients of Group 1 with controls, the difference of R² values in the substantia nigra obtained by ISQR was 3 and 4.4 s disease-related progression in PD as function of the disease duration. This is the main reason that led to develop the ISQR strategy with the aim of reducing large inter-subject variability (10–20 %) not related to disease in the regions of interest.

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Fig. 3. Heatmap of correlations between clinical features, R² values and R² values. The heatmap colors range is red when a significant positive correlation (P < 0.01), is orange when a significant positive correlation (P < 0.05), is dark green when a significant negative correlation (P < 0.01), is light green when a significant negative correlation (P < 0.05) and it is yellow when there is not significant: (A) R² raw values. (B) R² values. SN_D = substantia nigra_dominant; SN_ND = substantia nigra_non_dominant; RN_D = red nucleus_dominant; RN_ND = red nucleus_non_dominant; GPe = globus pallidusexternus_dominant; GPe = globus pallidusexternus_non_dominant; GPi = globus pallidus Internus_dominant; GPi = globus pallidus Internus_non_dominant; STR_D = striatum_dominant; STR_ND = striatum_non_dominant. MoCa = Montreal Cognitive Assessment, MDS-UPDRS = Movement Disorder Society-Unified Parkinson’s Disease Rating Scale, H&Y = Hoehn & Yahr score, S&E = Schwab & England score, MOGGQ = Freezing of Gait Questionnaire, LARS = Lille Apathy Rating Scale, HAM-D = Hamilton Rating Scale for Depression, HAM-A = Hamilton Rating Scale for Anxiety, ASBPD = Ardenin Scale of Behavior in Parkinson’s Disease, NMSS = Non-Motor Symptom Assessment Scale for Parkinson’s Disease, LEDD = Levodopa Equivalent Daily Dose. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)
control subjects. First, the inter-subject $R_2^*$ variability in the red nucleus was equivalent to the one measured in the other regions of interest. Secondly, we found that $R_2^*$ in the red nucleus and in the substantia nigra were highly correlated. Additionally, studies similar to ours did not find a difference in $R_2^*$ between parkinsonian patients and control subjects in the red nucleus (Barbosa et al., 2015; Martin and Gee, 2008; Murakami et al., 2015; Langkammer et al., 2016; Cheng et al., 2020) except in the work of Lewis (Lewis et al., 2013) who found an increase in the value of $R_2^*$ in parkinsonian patients with dyskinesia when compared to controls but no difference in Parkinson’s disease patients without dyskinesia when compared to controls. Unfortunately, no postmortem study is currently available to accurately assess the iron amount in red nuclei of patients with Parkinson’s disease. Due to the current lack of understanding, we cannot definitively say whether or not the red nuclei play a role in Parkinson’s disease. But our in vivo results bring several convincing results suggesting that choosing these nuclei as a reference is efficient to remove the $R_2^*$ variations unrelated to the disease.

As mentioned in the introduction, $R_2^*$ is not considered to be very sensitive biomarker, especially compared to the recent method based on the acquisition of T1-weighted neuromelanin (NM)-sensitive imaging. The study by Gaurav (Gaurav et al., 2021) showed variations of measured SN volume induced by Parkinson’s disease. The data published permitestimating the effect size at 0.76 in a diseased group (duration of progression <4 years) compared to a control group. In our R2* study, the effect size for group 1 (duration of progression <5 years) is 0.71/0.53 for dominant and non-dominant sides respectively, thus

Fig. 4. Two-dimensional plot based on principal component analysis. (A) Plot represents the relationships between the $R_2^*$ values of Parkinson’s disease patients and the clinical parameters included in this study. (B) Four distinct profiles of Parkinson’s disease patients according to the disease duration, illustrated by factorial analysis. The length of the arrows indicates the magnitude of the relationship to the $R_2^*$ values and clinical parameters, the first one (noted CompA1) was most related to severity of disease and the second (noted CompA2) to $R_2^*$ substantia nigra values. Each dot represents one Parkinson’s disease patient. (C) Plot represents the relationships between the $R_2^*$ values in the dominant side of Parkinson’s disease patients for each region of interest (D) Four distinct profiles of Parkinson’s disease patients according to the disease duration, illustrated by factorial analysis. The length of the arrows indicates the magnitude of the relationship to the $R_2^*$ values in substantia nigra (noted CompB1) whereas CompB2 expressed the magnitude of $R_2^*$ values whatever the region. Each dot represents one Parkinson’s disease patient. Parkinson’s disease = PD. The red color corresponds to PD patients > 15 years, the orange to PD patients > 10 and < 15 years, the yellow to PD patients > 5 and < 10 years and the green to PD patients < 5 years. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)
slightly less, pointing to lower sensitivity for the raw \(R^2\) approach compared to NM. However, using ISQR boosted the effect size which reached 1.50/1.12 for this group. This shows that ISQR is a pertinent means of increasing the sensitivity of the method based on \(R^2\) to the point of exceeding that of the T1-NM approach. Moreover, this increase in sensitivity linked to ISQR was confirmed for all the other groups (see Supplementary Information Table, Table 4).

4.3. Origin of \(R^2\) signal and variability

An interesting point to note is that for controls, neither the inter-subject \(R^2\) variations in the cortex nor those in the white matter are correlated with variations in subcortical regions (Supplementary Table 3). This is why these extended regions cannot serve as internal references for ISQR in the same way as the red nucleus do. In addition, since the inter-subject \(R^2\) variations in the subcortical regions are greater than in the rest of the brain and are strongly correlated, these variations probably originate from biological factors which specifically modify the \(R^2\) relaxation in these regions. Indeed, it is very unlikely that instrumental variations could explain such an inter-subject correlation of \(R^2\) specifically in subcortical regions.

It is therefore necessary to question the biological factors which are able to shift the \(R^2\) in the subcortical structures from one subject to another. Iron is undoubtedly the most important determinant of \(R^2\) relaxation in the human brain. To such an extent that initially, \(R^2\) mapping was suggested as an indicator of iron content (Gelman et al., 1999). Since iron is distributed in different forms at the cellular level, the relationship between iron concentration and \(R^2\) is not yet well established. The two major forms of iron are neuromelanin within the dopaminergic neurons and ferritin stored outside the dopaminergic neurons. Importantly, no particular hyperintensity was exhibited in the red nucleus using neuromelanin-weighted MRI (Trujillo et al., 2017). It can therefore be hypothesized that the \(R^2\) in the red nucleus and probably also in basal ganglia (i.e. striatum, globus pallidus) is mainly influenced by ferritin concentration. In sum, ferritin could be the biological factor which induces the inter-subject variations unrelated to Parkinson’s disease. Our results support this hypothesis and justify the use of the ISQR approach by taking the red nucleus as a reference to reflect the ferritin amount within the basal ganglia of each subject and thus emphasizing the variations due to neuromelanin.

Previous studies have shown that \(R^2\) does not only reflect the iron content. Experimental factors such as the orientation of the head in the scanner and small deviations of magnetic field strength can induce \(R^2\) variations (Azuma et al., 2016; Yablonskiy and Haacke, 1994; Li et al., 2012). Besides, due to the non-local nature of the magnetic field, \(R^2\) relaxation is prone to blooming artifacts, i.e. it depends both on local iron in a voxel and on the presence of other structures outside the voxel of interest which generate magnetic field variations due to susceptibility differences (Stüber and Wang, 2016). Due to the latter mechanism, \(R^2\) variations may partly be due to inter-subject differences of myelination (Duyn, 2017). This effect is unlikely to be significant here due to the absence of correlation between \(R^2\) in white matter and in subcortical regions.

4.4. Limitations-strengths

Many subjects were excluded from the current analysis after image quality control. As the number of patients with later stage Parkinson’s disease was limited, a contrast analysis between early-stage Parkinson’s disease subjects and later-stage Parkinson’s disease subjects was not performed. Moreover the MRI sequence was a fast multiple GRE which was prone to motion artifact and thus may explain the higher exclusion rate for patients, especially for later stages of disease evolution (see Fig. 1).

Obtaining quality acquisitions is a challenge since the propensity to perform abnormal movements during an exam (e.g., tremor, dyskinesia) is characteristic of Parkinsonian patients. Constant progress has been achieved in reducing the duration of sequences (e.g., 6min10s, Barbosa, J. H et al., 2015) since this acceleration reduces the possibility that a parasite movement of the patient occurs during acquisition. However, an intrinsic characteristic of high-speed sequences is the reduction of dead time, thus making more likely that a parasite movement occurs during an impactful period. Recent real time strategies based on suspending data acquisition during these periods are relevant (Castella et al., 2018) and could significantly improve the quality of \(R^2\) of future studies while reducing the level of rejection.

In our study, the red nucleus was chosen as a reference region for normalization because of its proximity to the substantia nigra, \(R^2\) values close to those of the substantia nigra, a lack of significant differences in \(R^2\) between patients and controls in this region in our study and in the majority of recent studies (Barbosa et al., 2015; Martin and Gee, 2008; Murakami et al., 2015; Langkammer et al., 2016; Cheng et al., 2020), except for differences reported by Lewis et al in patients with dyskinesia but not in patients without dyskinesia. However, when iron content in RN was assessed by quantitative susceptibility mapping (QSM), the reported results were contrasted with an increase in QSM signal (Sethi et al, 2019, Langkammer et al, 2016) or no significant variation (He et al, 2015, Azuma et al, 2016, Du et al, 2018). Furthermore, several studies have shown an increase in the volume of the RN in Parkinsonian patients (Colpan and Slavin, 2010; Camlidag et al 2014, Shah et al, 2020; Kolpakwar et al 2021) interpreted as a compensatory phenomenon linked to Parkinson’s disease, as the RN has many indirect and direct connections to motor coordinating pathways. Finally, and unfortunately, no post mortem data on RN in Parkinson’s disease is available, which limits our understanding of the role of this nucleus in the pathophysiology of Parkinson’s disease. Even if the involvement of RN in Parkinson’s disease is poorly understood, the magnitude of the disease’s effect on \(R^2\), if present, is small in this structure compared to that observed in SN. This is why this region can be chosen to serve as an internal reference.

In this paper, we present the results of our subjects at baseline. Our on-going longitudinal follow-up will be essential in confirming the dynamic changes of \(R^2\) during disease progression by applying the ISQR approach.

Performing MRI acquisitions in different centres and with various machines introduces further variability. In our study, MRI machines and sequences were normalized to reduce this instrumental variability. No differences were found between centres and machines. This validates the precautions taken for normalizing the acquisition protocol. However, many other instrumental factors impact data quality during the acquisition stage (choice of TEs, coils and sequences). Post-processing (motion correction, normalization, spatial filtering, region segmentation) (Fernandez-Seara, 2000; Kennan and Gore, 1994) affects data quality as well. If the proposed quantitative approach is based on proven open-access tools, it is very likely that the intra-subject variability can be further reduced by using up-to-date post-processing tools.

As clusters of substantia nigra pars compacta neurons are deeply embedded within the substantia nigra pars reticulata, the boundary between these two structures in humans is difficult to define, in particular in its caudal part (Prens and Parent, 2001). Moreover, spatial correspondence between histology and MRI of the substantia nigra at 1.5 and 3T is not precise (Lehericy et al., 2014). For this reason, we decided to refer to the substantia nigra as a whole for data analysis.

Considering that iron at the cellular level is distributed in different forms, this can presumably lead to distinct decaying behaviors as a function of TE, monoexponential for neuromelanin and quadratic exponential for ferritin (Krannichleh et al., 2018). Due to our limited range of echo times, these two lineshapes could not be disentangled. Thus, both contribute to the \(R^2\) obtained from the monoexponential fit.
A prerequisite when attempting to separate these two compartments would be to acquire low noise echo trains in a wider time range. This remains a challenge in clinical imaging conditions. Quantitative susceptibility mapping may be an alternative approach which appears to be more sensitive than using $R_2^*$ (Cheng et al., 2020). However, the susceptibility mapped by any technique is likely to be influenced by interindividual variability unrelated to the disease. Hence ISQR could improve this approach as well.

5. Conclusion

Our results indicate that $R_2^*$ mapping is a technique that can detect subtle iron-related variations in subcortical regions of Parkinson’s disease patients. However, certain conditions are necessary to eliminate variations not directly related to the disease. Both inter-subject variability and intra-subject variability, could explain the earlier, sometimes contradictory results obtained by quantitative MRI-$R_2^*$. Our ISQR strategy greatly improves the specificity of MRI-$R_2^*$ and designates $R_2^*$ a possible biomarker for monitoring the evolution of Parkinson’s disease.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Data availability

No data was used for the research described in the article.

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Appendix A

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Appendix B. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.nicl.2022.103231.

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Further reading

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