Increasing evidence highlights the importance of gross-total or maximal resection in improving survival in patients with glioblastoma. A number of techniques ranging from functional MRI and diffusion tensor imaging to transcranial magnetic stimulation have become popular in helping to identify the border of tumor and its relationship to regions of eloquent cortex. Anther primary tool in this repertoire is direct cortical and subcortical stimulation. Evidence has shown that there is considerable patient-to-patient variability with regard to eloquent cortex. In the presence of a mass lesion, there is also distortion/reorganization of anatomical pathways. For these reasons, cortical and subcortical mapping techniques have become fundamental during tumor resection to minimize damage to eloquent tissue.

Traditional bipolar stimulation is low-frequency (40–60 Hz) and uses a biphasic or balanced charge. This means that the stimulation at each electrode switches polarity halfway through to prevent leaving a net charge at the site of stimulation. When compared to monopolar stimulation, bipolar stimulation has been shown to cause less damage to tissue in animal models. However, a known complication of cortical bipolar stimulation is intraoperative seizures.

ABBREVIATIONS MEP = motor evoked potential; TOF = train-of-five.
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Use of the train-of-five bipolar technique to provide reliable, spatially accurate motor cortex identification in asleep patients

Evan D. Bander, MD,1 Evgeny Shelkov, BSN,2 Oleg Modik, PhD,2 Padmaja Kandula, MD,2 Steven C. Karceski, MD,2 and Rohan Ramakrishna, MD1

Departments of 1Neurosurgery and 2Neurology, NewYork-Presbyterian/Weill Cornell Medicine, New York, New York

OBJECTIVE Intraoperative cortical and subcortical mapping techniques have become integral for achieving a maximal safe resection of tumors that are in or near regions of eloquent brain. The recent literature has demonstrated successful motor/language mapping with lower rates of stimulation-induced seizures when using monopolar high-frequency stimulation compared to traditional low-frequency bipolar stimulation mapping. However, monopolar stimulation carries with it disadvantages that include more radiant spread of electrical stimulation and a theoretically higher potential for tissue damage. The authors report on the successful use of bipolar stimulation with a high-frequency train-of-five (TOF) pulse physiology for motor mapping.

METHODS Between 2018 and 2019, 13 patients underwent motor mapping with phase-reversal and both low-frequency and high-frequency bipolar stimulation. A retrospective chart review was conducted to determine the success rate of motor mapping and to acquire intraoperative details.

RESULTS Thirteen patients underwent both high- and low-frequency bipolar motor mapping to aid in tumor resection. Of the lesions treated, 69% were gliomas, and the remainder were metastases. The motor cortex was identified at a significantly greater rate when using high-frequency TOF bipolar stimulation (n = 13) compared to the low-frequency bipolar stimulation (n = 4) (100% vs 31%, respectively; p = 0.0005). Intraoperative seizures and afterdischarges occurred only in the group of patients who underwent low-frequency bipolar stimulation, and none occurred in the TOF group (31% vs 0%, respectively; p = 0.09).

CONCLUSIONS Using a bipolar wand with high-frequency TOF stimulation, the authors achieved a significantly higher rate of successful motor mapping and a low rate of intraoperative seizure compared to traditional low-frequency bipolar stimulation. This preliminary study suggests that high-frequency TOF stimulation provides a reliable additional tool for motor cortex identification in asleep patients.

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KEYWORDS intraoperative motor mapping; bipolar; train-of-five; seizure; stimulation
cause injury and require prompt treatment with application of ice-cold saline and/or rapid administration of benzodiazepines or antiepileptics, but they can also preclude further functional mapping. Moreover, bipolar stimulation may fail to identify the motor cortex in a diseased brain. The use of monopolar high-frequency (250–500 Hz), train-of-five (TOF) stimulation has recently been shown to deliver reliable motor and language mapping while causing decreased seizure activity. The main theoretical disadvantage to monopolar TOF stimulation is diffuse, radial spread of electrical stimulation that leads to spatially inaccurate motor cortex identification.

We provide a third possibility, one that combines the two: anodal TOF stimulation delivered between two electrodes. This can be done using a traditional bipolar wand or using two electrodes of a subdural strip that is placed in the surgical field, immediately adjacent to the area of resection. With this technique, we hope to deliver highly reliable TOF stimulation but in a more focused way akin to low-frequency bipolar stimulation. This case series contrasts the use of high-frequency bipolar TOF stimulation with low-frequency bipolar cortical stimulation during intraoperative mapping. Two variables were of primary interest: 1) the ability to map the motor cortex and 2) the occurrence of intraoperative seizures.

**Methods**

This study was approved by the Institutional Review Board at Weill Cornell Medical College. A retrospective chart review was completed to identify demographic data, pathology, intraoperative stimulation data, preoperative and intraoperative seizure status, and postoperative surgical complications. Between 2018 and 2019, 13 patients underwent motor mapping with phase-reversal and both low- and high-frequency bipolar stimulation.

**Intraoperative Monitoring Techniques**

Standard neurosurgical approaches, including the use of intraoperative neuronavigation and ultrasound, were used to identify the tumor location and to perform a craniotomy appropriately tailored for the resection. A Cascade Elite machine (Cadwell) was used for all neuromonitoring modalities.

Once the dura mater was open, several intraoperative modalities were employed. First, median nerve stimulation “phase reversal” was accomplished using a 6- or 8-contact subdural electrode (Ad-Tech Medical; 10-mm contact spacing), placed perpendicular to the central sulcus. When present, the phase reversal confirmed the location of the central sulcus, thereby identifying the gross anatomical location of the motor cortex with respect to the tumor (Fig. 1). Subsequently, direct cortical stimulation motor mapping was performed in two ways (Table 1). First, high-frequency TOF bipolar stimulation was delivered using a TCS-4 stimulator (Cadwell) and a handheld neural probe (Double Ball Tip Probe, Cadwell). Needle recording electrodes monitored the motor response. The intensity of the stimulation was increased systematically until a motor evoked potential (MEP) was elicited, establishing a threshold for the MEP response. The subdural strip of electrodes was used to monitor afterdischarges or
evoked intraoperative seizures. Following this, using the same handheld neural stimulator probe, low-frequency (50-Hz) bipolar simulation was applied with a Nicolet Cortical Stimulator (Natus Neuro). A motor response was documented by clinical observations (observable muscle movements) and by recording a motor response in the needle recording electrodes.

After confirmation of the motor cortex location, attention was turned to the resection. During the resection, subthreshold direct cortical MEP responses were elicited every 2–15 seconds, using the subdural electrode strip. In this way, MEP responses could be monitored throughout the resection. Electrophysiology monitoring was completed by a specialty-trained neurologist and staff.

**Statistical Analysis**

Two-sample proportion Fisher’s exact test was used to calculate probability values for categorical variables, including the rate of positive motor mapping and intraoperative seizure frequency. A p value < 0.05 was considered statistically significant. Microsoft Excel (Microsoft Corp.) and GraphPad Prism (GraphPad Software) were used for statistical analysis.

**Results**

A total of 13 patients (6 men and 7 women) underwent both high- and low-frequency bipolar motor mapping (Table 2). The mean patient age was 51 years (range 26–79 years). The majority of patients (69%) had gliomas, and the remainder had metastatic tumors. Seizure was the most common presenting symptom in this cohort. The mean follow-up duration was 165 days (range 5–541 days).

Table 2 demonstrates the demographics of the cohort.

The motor cortex was identified at a significantly greater rate when using the high-frequency TOF bipolar stimulator (n = 13) compared to the low-frequency bipolar stimulator (n = 4) (100% vs 31%, respectively; p = 0.0005) (Table 3). The mean maximum stimulation intensity for the low-frequency stimulation was 8 ± 2.2 mA (range 4–12 mA) and that for high-frequency TOF stimulation was 53 ± 17.7 V (range 40–100 V). Low-frequency stimulation was successful at eliciting an MEP in 44% of the patients with gliomas (n = 4) but in 0% of the patients with metastatic tumors (p = 0.22). All patients underwent continuous MEP monitoring throughout the procedure without intraoperative decrement. Five patients (38%) had postoperative deficits, including supplementary motor area syndrome (n = 3), neglect (n = 1), or new postoperative weakness (n = 1). There were no ischemic strokes. Of the 5 patients with postoperative deficits, 2 had successfully elicited MEPs with both high- and low-frequency stimulation prior to resection. All of the postoperative deficits were improved at subsequent follow-up visits.

Intraoperative seizures (n = 2) occurred only in the low-frequency bipolar group, and no seizures occurred in the TOF group, but this did not reach statistical significance (15% vs 0%, respectively; p = 0.48). Afterdischarges were identified in 2 patients in the low-frequency group, which, when combined with intraoperative seizures, trended toward a significantly higher rate in the low-frequency compared to high-frequency group (p = 0.096). Both patients

**TABLE 1. Stimulation parameters**

| Parameter                        | Low-Frequency Stimulation | High-Frequency Stimulation |
|----------------------------------|----------------------------|----------------------------|
| Pulse                            | Biphasic, rectangular, 50 Hz | TOF pulses                 |
| Pulse width                      | 0.05–0.075 msec            | 0.5 msec                   |
| Intensity                        | 2–4 mA (peak to peak)      | 10–100 V                   |
| Polarity                         | Bipolar                   | Anodal                     |
| Stimulation duration/interstimulus interval | 1–6 sec/NA                | NA/3 msec                  |

NA = not applicable.

**TABLE 2. Patient demographics**

| Characteristic | Value | %       |
|----------------|-------|---------|
| Mean age, yrs | 51 ± 15.9 |        |
| Total no. of patients | 13 |        |
| Male            | 6 | 46.2    |
| Female          | 7 | 53.8    |
| Pathology       |   |         |
| Glioblastoma    | 6 | 46.2    |
| Low-grade glioma | 3 | 23.1    |
| Metastasis      | 4 | 30.8    |
| Surgical side   |   |         |
| Right            | 8 | 61.5    |
| Left             | 5 | 38.5    |
| Tumor location  |   |         |
| Frontal          | 7 | 53.8    |
| Parietal         | 6 | 46.2    |
| Presenting symptom |   |         |
| Asymptomatic     | 2 | 15.4    |
| Numbness/tingling | 3 | 23.1    |
| Seizure          | 5 | 38.5    |
| Weakness         | 3 | 23.1    |
| Preoperative seizures | 7 | 53.8    |
| Preoperative motor deficit | 5 | 38.5    |
| Mean follow-up, days (range) | 165 (5–541) |        |

*Values are expressed as the number and percentage of patients unless otherwise indicated.*

**TABLE 3. Operative outcomes**

| Characteristic | Low-Frequency Bipolar Stimulation | TOF Bipolar Stimulation |
|----------------|----------------------------------|-------------------------|
| Positive MEP   | 4 (30.8%)                        | 13 (100%)*              |
| Intraoperative seizure | 2 (15.4%) | 0 (0%)                   |
| Mean max stimulation | 8 ± 2.2 mA | 53 ± 17.7 V             |
| Postoperative deficit | 5 (38%)  |                         |

* Two-sample proportional Fisher exact method, p < 0.05.
who experienced intraoperative seizures had a history of preoperative seizures.

Discussion

Motor mapping has become an integral part of safe and maximal tumor resections. The origin of motor mapping can be traced primarily to the work of Wilder Penfield in the 1930s. Using 60-Hz stimulation over 1- to 6-second impulses, Penfield was able to elicit movements, sensations, or language interruption in patients.21,38 This form of stimulation, however, resulted in significant afterdischarges and seizures. The technique was advanced when Berger, Yingling, and Ojemann demonstrated that significantly lower stimulation intensities could elicit changes in monitored electromyography activity.38,39 The traditional bipolar method for motor and language mapping can limit motor deficits by halting resection at a minimum of 1 cm from positive stimulation points.11 The main drawback of this technique has been a concern for a high rate of intraoperative seizures. The seizure rate varies between 3% and 20% in the literature.1,25,30,34,39 It is worth noting that a recent report by Boetto et al. suggested that the rate of intraoperative seizures when using low-frequency bipolar stimulation can be reduced to less than 5%.2 They demonstrated preparation of a larger craniotomy to permit visualization of the motor cortex and subsequent stimulation threshold determination through elicitation of electromyography activity and anarthria via stimulation of the motor cortex and ventral premotor cortex, respectively. No electrocorticography was used. They had positive language mapping in all cases with low seizure rates, suggesting that stimulation threshold determination through afterdischarge monitoring may not be necessary. Their results further suggest that the stimulation threshold determined from the motor and ventral premotor cortex is reliable for subsequent language mapping use. Our report differs from this study in important ways. First, our study aimed to assess the role of high-frequency TOF stimulation in asleep patients for motor cortex identification only. The relevance of this technique in language mapping is unclear. Second, our study indicates that high-frequency TOF stimulation is an additional, safe, reliable tool for motor cortex identification, which can be challenging in patients with distorted cortical anatomy and tumors associated with vasogenic edema.

Monopolar high-frequency TOF stimulation was first introduced in 1993 by Taniguchi et al.36 Using high-frequency impulses with short interstimulus intervals allowed for an accumulation of excitatory postsynaptic potentials in motor neurons. This method theoretically requires fewer impulses than low-frequency stimulation, which is delivered over longer periods of time. As such, TOF stimulation theoretically delivers a lower charge density and less potential for tissue damage.36 The high-frequency stimulation technique, on further testing, has been successfully used for motor and language mapping.2,4,14,15,24,31 Comparing the different stimulation techniques, monopolar high-frequency stimulation has been found to require a lower relative stimulation intensity to achieve a positive MEP.25 However, the success of high-frequency stimulation is greatest for mapping of the primary motor cortex and has been found to be less sensitive than bipolar mapping for identifying motor responses in the premotor frontal cortex and supplementary motor areas.15 This may be due to the higher density of pyramidal neurons in the primary motor cortex compared to the supplementary motor areas. Importantly, high-frequency stimulation is able to achieve successful mapping with low rates of intraoperative seizure, ranging between 0% and 3%.24,37

Our case series examined the advantages of high-frequency TOF stimulation delivered using a bipolar electrode, compared with the more traditional low-frequency stimulation. Using this technique, we achieved a significantly higher rate of positive stimulation sites and a low rate of intraoperative seizures. Of the 5 transient neurologic deficits that occurred, 2 were in patients who had positive stimulation when using both TOF and low-frequency techniques, and 3 were in patients who had only positive TOF stimulation mapping. Patients who had positive sites with both high- and low-frequency techniques had concordant localization of the motor cortex. All of the motor sites identified by only positive TOF motor localization were in agreement with phase reversal and gross anatomical localization. Since no deficit was permanent or severe and all improved, these were not considered related to inaccurate motor mapping, but rather were deficits secondary to postoperative edema or injury to supplementary motor areas.26 In previous studies, monopolar stimulation, with either high- or low-frequency stimulation, had been demonstrated to achieve higher rates of eliciting an MEP while at lower thresholds than bipolar stimulation.35 However, monopolar stimulation has a radiant spread that can decrease spatial accuracy, given the typically distant placement of the reference electrode. By using a bipolar wand, where one of the electrodes serves as the reference, our results indicate that high-frequency TOF stimulation can provide spatially accurate motor mapping with extremely low rates of seizures and acceptable postoperative morbidity. It is difficult to confirm whether our higher rate of positive stimulation with the TOF technique was due to a true increase in sensitivity or was actually a false positive. However, given the appropriate correlation of our positive bipolar TOF mapping sites with modalities, such as phase reversal and anatomical landmarks, we favor these sites to be true positives. In addition, although the total number of concordant cases was low for TOF and low-frequency mapping, in those cases there was strong concordance of the positive sites between traditional low-frequency bipolar stimulation and our technique. This suggests that high-frequency TOF stimulation does indicate positive cortical motor sites. Ultimately, this preliminary report points to an additional reliable technique to identify motor cortex.

Our series is limited by the lack of comparison with a monopolar TOF stimulation, potential unconscious bias, lack of blinding, and the small sample size limiting the power of the study. Ideally, our study would have also elucidated the reliability of monopolar TOF mapping of the motor cortex. A future prospective study may further clarify its role. However, some caution may be advisable in a study looking at multiple electrical stimulation techniques given the increased operative time and the increased theo-
It is important to note that there did not appear to be variability in the identification of the motor cortex when both techniques produced positive results. As such, our technique provides an additional reliable modality that reinforces the crucial role of intraoperative mapping for the determination of safe operative corridors and complete tumor resections. Based on our experience, we believe bipolar TOF stimulation is capable of achieving excellent motor mapping with minimal spread, few afterdischarges or seizures, and low rates of permanent postoperative deficits.

Conclusions

Using a bipolar wand with high-frequency TOF stimulation, we achieved a significantly higher rate of successful motor mapping, as well as a low rate of intraoperative seizure compared to traditional low-frequency bipolar stimulation. This preliminary study suggests that high-frequency TOF stimulation provides a reliable additional tool for motor cortex identification in asleep patients. Further comparison studies of motor mapping techniques are required, and a true gold standard for calculating sensitivity and specificity should be defined.

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Author Contributions
Conception and design: Ramakrishna, Bander, Kandula, Karczeski. Acquisition of data: all authors. Analysis and interpretation of data: all authors. Drafting the article: Ramakrishna, Bander, Shelkov, Modik, Karczeski. Critically revising the article: Ramakrishna, Bander, Shelkov, Kandula, Karczeski. Reviewed submitted version of manuscript: Ramakrishna, Bander, Karczeski. Approved the final version of the manuscript on behalf of all authors: Ramakrishna. Statistical analysis: Ramakrishna, Bander. Study supervision: Ramakrishna.

Correspondence
Rohan Ramakrishna: Weill Cornell Medical College, New York, NY. ror9068@med.cornell.edu.