Differentiating novel coronavirus pneumonia from general pneumonia based on machine learning

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Research

Keywords: Machine learning, Novel coronavirus pneumonia, General pneumonia, Chest CT

Posted Date: August 14th, 2020

DOI: https://doi.org/10.21203/rs.3.rs-31313/v3

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Version of Record: A version of this preprint was published on August 19th, 2020. See the published version at https://doi.org/10.1186/s12938-020-00809-9.
Abstract

**Background:** Chest CT screening as supplementary means is crucial in diagnosing novel coronavirus pneumonia (COVID-19) with high sensitivity and popularity. Machine learning was adept in discovering intricate structures from CT images and achieved expert-level performance in medical image analysis.

**Methods:** An integrated machine learning framework on chest CT images for differentiating COVID-19 from general pneumonia (GP) was developed and validated. Seventy-three confirmed COVID-19 cases were consecutively enrolled together with twenty-seven confirmed general pneumonia patients from Ruian People's Hospital, from January 2020 to March 2020. To accurately classify COVID-19, region of interest (ROI) delineation was implemented based on ground glass opacities (GGOs) before feature extraction. Then, 34 statistical texture features of COVID-19 and GP ROI images were extracted, including 13 gray level co-occurrence matrix (GLCM) features, 15 gray level-gradient co-occurrence matrix (GLGCM) features and 6 histogram features. High dimensional features impact the classification performance. Thus, ReliefF algorithm was leveraged to select features. The relevance of each features was the average weights calculated by ReliefF in n times. Features with relevance larger than the empirically set threshold T were selected. After feature selection, the optimal feature set along with 4 other selected feature combinations for comparison were applied to the ensemble of bagged tree (EBT) and four other machine learning classifiers including support vector machine (SVM), logistic regression (LR), decision tree (DT), and K-nearest neighbor with Minkowski distance equal weight (KNN) using 10-fold cross-validation.

**Results and Conclusions:** The classification accuracy (ACC), sensitivity (SEN), specificity (SPE) of our proposed method yield 94.16%, 88.62% and 100.00%, respectively. The area under the receiver operating characteristic curve (AUC) was 0.99. The experimental results indicate that the EBT algorithm with statistical textural features based on GGOs for differentiating COVID-19 from general pneumonia achieved high transferability, efficiency, specificity, sensitivity, and impressive accuracy, which is beneficial for inexperienced doctors to more accurately diagnose COVID-19 and essential for controlling the spread of the disease.

**Background**

Since the first COVID-19 case was discovered in 2019, more than 9.47 million cases of novel coronavirus pneumonia have been diagnosed worldwide, with 484,249 deaths recently according to World Health Organization Coronavirus disease (COVID-2019) situation report - 158. Currently, the detection of COVID-19 mainly relies on nucleic acid testing. However, many infected patients with obvious typical symptoms passed multiple nucleic acid tests but diagnosed positive in the last test\(^1\). The high false negative rate results in delayed treatment and even aggravating the spread of the pandemic. On February 5, the Chinese National Health and Health Commission launched the "Novel Coronavirus Pneumonia Diagnosis and Treatment Program (Trial Version 5)\(^1\)", which updated the diagnostic criteria for novel coronavirus pneumonia with adding CT imaging examinations as one of the main basics for clinical diagnosis of
COVID-19. CT screening is considerably popular, easy to operate and sensitive to COVID-19, which is critical for both early diagnosis and pandemic control.

Nevertheless, influenza virus pneumonia and other types of pneumonia might occur in this season as well. In some aspects, especially according to clinical features, it is troublesome to differentiate COVID-19 from general pneumonia. For instance, the main manifestations of COVID-19 in the early stage were fever, fatigue, dry cough, and expiratory dyspnea while patients with general pneumonia have similar symptoms\(^2\). COVID-19 pneumonia places a huge burden on the health care system because of its high morbidity and mortality. Therefore, early diagnosis and isolation of GP patients and COVID-19 patients can better prevent the spread of the pandemic and optimize the allocation of medical resources. However, except for the overlapping symptoms and detection abnormalities, CT manifestations of GP and COVID-19 were similar, causing instability and uncertainty for distinguishing them\(^3,4\).

Typical CT manifestations of COVID-19 patients consist of pleural indentation sign, unilateral or bilateral pulmonary ground-glass opacities, opacities with rounded morphology and patchy consolidative pulmonary opacities with the predominance in the lower lung\(^5-8\). GP infections have similar CT manifestations at presentation. However, COVID-19 presents more bilateral extensive GGO while GP shows more unilateral GGO or consolidation\(^9\). Furthermore, the other CT funding of GP and COVID-19 and GP is difficult to be observed and the areas of lungs contain larger scale of insignificant extraneous parts. To avoid the interference of irrelevant information and more accurately and stably identify COVID-19 from GP, GGO was cropped as the region of interest (ROI) and features were extracted based on ROIs. Figure 1 shows the samples of COVID-19 and GP CT images from the collected dataset.

Lin et al. proposed a deep learning model, COVNet, based on visual features from volumetric CT images to distinguish COVID-19 from community acquired pneumonia\(^10\). 4536 three-dimensional CT images (COVID-19: 30%; Community Acquired Pneumonia: 40%; non-pneumonia: 30%) were included in their study. U-net was applied to crop the lung region as the ROI and both 2D and 3D features were extracted by COVNet based on the ROIs. Then the features were combined and input into the proposed scheme for predictions. The sensitivity and specificity for detecting COVID-19 were 90% and 96% while for CAP were 87% and 92%. The AUCs were 0.96 and 0.95. However, due to the deep learning method, which feature determines the result stays unknown. Thus, the method lacks of interpretability and transparency.

Charmaine et al. evaluated ResNet with a location-attention mechanism model for screening COVID-19\(^11\). Two ResNet models were enrolled in their study. Three-dimensional features were extracted by ResNet-18 and fed into ResNet-23 with location-attention mechanism in the full-connected layer for classification while ResNet without location-attention mechanism was applied as well for comparison with the proposed method. Accordingly, the results show the proposed method achieved better performance with an overall accuracy of 86.7%.

Asif et al. proposed CoroNet model based on Xception architecture using X-ray images to differentiate COVID-19 from healthy, bacterial pneumonia and viral pneumonia\(^12\). Notably, Xception is a transfer
learning model which was pertained on ImageNet dataset and then retained on the collected X-ray dataset. In the proposed architecture, the classical convolution layers were replaced by convolutions with residual connections. The overall accuracy was 89.6% while average accuracy of detecting COVID-19 was 96.6%. To test the stability and robustness, CoroNet was evaluated on the dataset prepared by Ozturk et al\textsuperscript{13} with an accuracy of 90%.

Ozturk et al. developed DarkNet model based on the you only look once (YOLO) system to detect and classify COVID-19\textsuperscript{13}. Their model achieved the accuracy of 98.08\% for classifying COVID-19 and non-infections and 87.02\% for distinguish COVID-19 from COVID-19, no-findings and GP. Nevertheless, the proposed methods by Asif et al. and Ozturk et al. were based on X-ray images. X-ray screening is not sensitive to GGOs which is one of the most significant manifestations at the early stages of COVID-19. This can cause high error rate and ineffective containment of the pandemic.

Kang et al. developed a machine learning method with structured latent multi-view representation learning to diagnose COVID-19 and community acquired pneumonia\textsuperscript{14}. In their work, V-Net was leveraged to extract lung lesions. Then, radiomic features and handcrafted features, totally 189-dimentional features, were extracted from the CT images. In the end, the proposed model yielded the best accuracy, which was 95.50\%. The sensitivity and specificity were 96.6\% and 93.2\%. Compared with other methods in the study, the accuracy was improved by 6.1\%~19.9\% and the sensitivity and specificity were improved by 4.61\%~21.22\%.

To our knowledge, most recent researches carried out for detecting COVID-19 are based on deep learning. However, deep learning models require a large scale of training data while initially the COVID-19 samples are in shortage. Transfer learning might be promising method in terms of small amount of data while negative transfer may exist, for initial dataset and target domains may not related to each other and the standards on what types of training data are sufficiently related are not clear.

Machine learning plays an insubstitutable role in artificial intelligence with outstanding results in medical imaging classification. We developed a machine learning method using ensemble of bagged tree based on statistical texture features of CT images, particularly focusing on differentiating COVID-19 from GP, demonstrating high efficiency in the identification of COVID-19 and GP, helping to reduce misdiagnosis and control pandemic transmission.

**Material**

From January 2020 to March 2020, there were 73 COVID-19 cases confirmed by nucleic acid test positive and 27 general pneumonia cases enrolled in this study (age ranges from 14 to 72 years). Both COVID-19 and GP patients who had undergone chest CT scans were retrospectively reviewed by two senior radiologists. Of the COVID-19 cases, twelve patients without obvious characteristics on CT images were excluded (negative rate 16.4\%, 12/73). Finally, sixty-one confirmed COVID-19 cases and 27 general pneumonia cases were enrolled in this study.
The images were independently assessed by two radiologists. If the radiologists disagreed with each other, a senior radiologist would be invited to review the pulmonary CT images and make the final examination. All the CT images were generated from the Siemens Sensation 16-layer spiral CT (Siemens, Erlangen, Germany). The image format was Digital Imaging and Communications in Medicine (DICOM). The scan parameters were: tube voltage 120 kV; tube current automatic regulation; 1-2 millimeters cross-sectional thickness; 1-2 millimeters cross-sectional distance; scan pitch 1.3; and 16×0.625 millimeters collimation.

**Results**

The proposed diagnosis method is ensemble of bagged trees based on feature combination 5(T=0.11) including ROI delineation, feature extraction, feature selection and classification which are explicitly described in method section. In this section, the results of feature selection, effectiveness of optimal feature combination 5 compared to original features, and comparison of EBT algorithm and four other classification methodologies are described. The experimental result demonstrated that the proposed COVID-19 diagnosis method outperformed other methods in terms of accuracy, sensitivity, specificity and AUC.

**Results of feature selection**

Table 1 and figure 2 show the relevance of each feature and weight curves of each feature based on ReliefF algorithm. In order to select the optimal feature combination, the proposed threshold T was set to 0.11. To justify optimization, combination 1(T=0.11*), combination 2(T=0.12), and combination 3(T=0), combination 4(T=0.10) were considered to compare with combination 5(T=0.11). Features included according to four different T values are shown in Table 2(The corresponding feature names of the feature numbers are presented in Table 4 in the method section).

| feature | relevance | feature | relevance | feature | relevance | feature | relevance | feature | relevance |
|---------|-----------|---------|-----------|---------|-----------|---------|-----------|---------|-----------|
| 1       | 0.0421    | 8       | 0.1329    | 15      | 0.0043    | 22      | 0.1348    | 29      | 0.1250    |
| 2       | 0.1036    | 9       | 0.1338    | 16      | 0.0687    | 23      | 0.1257    | 30      | 0.1025    |
| 3       | 0.0050    | 10      | 0.1059    | 17      | 0.0548    | 24      | 0.1170    | 31      | 0.1490    |
| 4       | 0.0178    | 11      | 0.0582    | 18      | 0.1604    | 25      | 0.1574    | 32      | 0.1250    |
| 5       | 0.0032    | 12      | 0.0360    | 19      | 0.1574    | 26      | 0.2267    | 33      | 0.0389    |
| 6       | 0.1434    | 13      | 0.0163    | 20      | 0.2561    | 27      | 0.2977    | 34      | 0.0963    |
| 7       | 0.1036    | 14      | 0.1184    | 21      | 0.1469    | 28      | 0.2094    |         |           |

The X axis represents the numbers of features. The Y axis represents the weights of different features at different times. The algorithm run 1000 times represented by curves with different colors. The dark straight line represents weight = 0.11, which is the proposed threshold T.
Table 2 Selected features of four combinations

| Combination | T      | Feature numbers                  |
|-------------|--------|----------------------------------|
| 1           | 0.11*  | 1,2,3,4,5,7,10,11,12,13,15,16,17,30,33,34 |
| 2           | 0#     | All 34 features                  |
| 3           | 0.10   | 2,6,7,8,9,10,14,18,19,20,21,22,23,24,25,26,27,28,29,30,31,32 |
| 4           | 0.12   | 6,8,9,18,19,20,21,22,23,25,26,27,28,29,31,32 |
| 5           | 0.11   | 6,8,9,14,18,19,20,21,22,23,24,25,26,27,28,29,31,32 |

*select features with relevance smaller than the threshold T.
*No feature selection was applied.

Performance Evaluation

Table 3 shows the diagnosis performance of 5 classifiers based on 5 different feature combinations. In order to intuitively present the differences in accuracy, sensitivity and specificity of different methods using different feature combinations, we visualized them with line figure 3, line figure 4 and line figure 5 respectively. The receiver operating characteristic (ROC) curves of EBT algorithm and 4 other classifiers using the optimal feature combination 5 were presented in figure 6.

1) Effectiveness of optimal feature combination 5 compared to original features

Figure 3 elucidates that five classifiers using feature combination 5 achieved the highest accuracy than that obtained by other feature combinations. The measurements in the X-axis ranging from 1 to 5 represents the sequence numbers of the combinations. Figure 4 and 5 substantiates that the sensitivity and specificity of the optimal feature set outperformed that of combination 2 as well as combination 1, 3 and 4. To be noted, combination 2 contains 34 features which indicates that no feature selection was applied, which illustrates that feature selection is essential.

2) Comparison of EBT and four other classification methodologies

As shown in table 3, the best result are obtained by EBT algorithm with feature combination 5, leading to accuracy, sensitivity and specificity of 94.16%, 88.62% and 100.00%, respectively. Three line figures reveals that EBT algorithm achieved clearly better performance compared with other classification methodologies using no matter what feature combinations. Figure 6 demonstrates ROC curves of five models based on feature combination 5. And the AUCs (area under curve, AUC) of DT, LR, SVM, KNN and EBT are 0.91, 0.88, 0.94, 0.88, and 0.99, respectively. The EBT provides the best AUC. Therefore, the promising results validate that the proposed method can accurately and robustly differentiate COVID-19 from GP.

Table 3 Diagnosis performance based on different methods using different combinations
| Method | Combination 1 | Combination 2 | Combination 3 | Combination 4 | Combination 5 |
|--------|---------------|---------------|---------------|---------------|---------------|
| DT     | 81.98         | 88.82         | 89.41         | 89.73         | 89.82         |
|        | 72.03         | 85.85         | 84.34         | 84.39         | 85.90         |
|        | 80.40         | 91.95         | 95.64         | 95.55         | 95.69         |
| LR     | 70.64         | 80.57         | 81.65         | 79.15         | 81.73         |
|        | 66.50         | 76.42         | 77.89         | 75.61         | 77.89         |
|        | 75.00         | 84.93         | 85.62         | 82.88         | 85.73         |
| VM     | 81.90         | 85.32         | 85.65         | 86.07         | 86.48         |
|        | 76.91         | 83.58         | 82.11         | 81.30         | 83.79         |
|        | 87.16         | 87.16         | 89.38         | 91.10         | 91.44         |
| NN     | 77.73         | 83.23         | 85.40         | 88.32         | 88.24         |
|        | 69.43         | 73.98         | 79.51         | 81.79         | 82.33         |
|        | 86.47         | 92.97         | 91.61         | 95.21         | 96.58         |
| BT     | 86.49         | 92.91         | 92.49         | 93.41         | 94.16         |
|        | 78.37         | 86.18         | 85.69         | 87.32         | 88.62         |
|        | 95.03         | 100.00        | 99.66         | 99.83         | 100.00        |

**Discussion**

The proposed diagnosis method was evaluated in term of accuracy, sensitivity and specificity. As shown in equation 2-4 in the method section, accuracy measures the ability of the diagnosis system to correctly detect COVID-19 and GP. Sensitivity demonstrates the proportion of correctly classified COVID-19 cases. Specificity illustrates how good the method is at identifying GP cases. As shown in table 3, the highest accuracy, sensitivity and specificity achieved by EBT algorithm with feature combination 5 were 94.16, 88.62, and 100.00, respectively. It shows that the proposed method did better performance in detecting GP than COVID-19. To alleviate class imbalance, we did data augmentation on GP images. However, data augmentation techniques cannot increase the diversity of GP features. Although the proposed method achieved the specificity of 100.00%, which suggests no GP cases were erroneously classified, there is no denying that it has the probability of over-fitting caused by shortage in GP images.

CT of COVID-19 infections presents consolidation, GGO, pulmonary fibrosis, interstitial thickening, and pleural effusion in both lungs \(^{15-17}\) while CT of GP infections presents multifocal nodular opacity with a surrounding halo, diffuse patchy GGO, interlobular septal thickening, multiple ill-defined nodules and consolidation in both lungs \(^{18}\). Thus, most recent researches have proposed heterogeneous methods based on the whole lung region. For example, Wang et al. developed COVID-19Net for diagnosing COVID-19 with automatic lung segmentation of CT images using DenseNet121-FPN \(^{19}\). Notably, DenseNet121-FPN is also a transfer learning framework, which was pre-trained on ImageNet dataset as well. The sensitivity and specificity of the method were 78.9% and 89.93% in the training set. In the two validation sets, the sensitivities were 80.39% and 79.35% and the specificities were 76.61% and 81.16%. As mentioned previously in the background section, the deep learning method proposed by Lin et al. implemented U-net for lung segmentation \(^{10}\). It achieved the sensitivity and specificity of 90% and 96%. Zhang et al. used AI system with a two-stage segmentation framework to segment lung lesions and then diagnose COVID-19 \(^{20}\). The first stage of the segmentation framework was manually annotation and the
second stage was DeepLabv3-based backbone for lung lesion segmentation. In their work, they achieved smoother and clearer boundaries compared with experts. Besides, they validated their system in the dataset from outside China with 84.11% accuracy, 86.67% sensitivity, and 82.26% specificity for differentiating COVID-19 from GP. Wu et al. developed a multi-view deep learning fusion model based on the architecture of ResNet50 with threshold segmentation and morphological optimization algorithms for lung segmentation. The accuracy, sensitivity and specificity of their model in the testing set were 0.760, 0.811 and 0.615 respectively. However, compared with these studies, we did GGO segmentation instead of lung lesion segmentation. Our proposed machine learning method in combination with GGO segmentation accomplished the accuracy of 94.16% for distinguish COVID-19 from GP. It also has a high sensitivity and specificity of 88.62% and 100.00% respectively. Therefore, we achieved better performance in diagnosing COVID-19 based on only GGOs. The results empirically validate that COVID-19 and GP can be robustly classified based on GGOs.

Despite the remarkable performance of the proposed methods, limitations still exist in our study. First of all, the ROIs were manually delineated which is rather time-consuming especially when doctors are racing against time to save lives. Also, GGOs were the exclusive segmented features of CT images of COVID-19 and GP and spending more time on ROI segmentation is apparently unworthy while the whole lung region contains irrelevant or even pernicious information for diagnosis. Hence, further study should be processed on automatically and precisely detect and segment ROIs without manually help. Finally, our established model didn’t determine which specific general pneumonia it was, such as viral or bacterial, mainly due to insufficient data. More data will be collected and the prognosis of GPs will be considered in our future study.

**Conclusions**

This study explored an ensemble of bagged tree algorithm with statistical textural features for differentiating novel coronavirus pneumonia from general pneumonia. The classification accuracy, sensitivity, and specificity of our proposed method yield 94.16%, 88.62% and 100.00%, respectively. Furthermore, GGOs were proved to play a significant role in distinguish COVID-19 from GP. The results show that classifiers with feature selection excelled classifiers without feature selection by 1%-5% for accuracy, 2%-10% for sensitivity and 0%-4% for specificity. More importantly, classifiers with feature selection take shorter time. In conclusion, the experimental results show that, as compared to other state-of-the-art works, the proposed method achieved pronouncedly superior performance with a small amount of CT images.

**Methods**

**Overview of the proposed diagnosis framework**

Machine learning algorithms integrated with statistical textural features are leveraged to differentiate COVID-19 from GP. Figure 7 illustrates the block diagram of the proposed diagnosis framework. After
data collection, to more accurately extract features of COVID-19 and GP, manually delineation of the ROIs were performed based on GGOs. The details of ROI delineation are presented in Delineation of ROIs section. In the next step, 34 statistical texture features including 13 GLCM features, 15 GLGCM features and 6 histogram features were extracted from the ROIs. After that, ReliefF algorithm was used to select features for time-saving and avoiding over-fitting. As a result, five feature combinations were remained while combination 5 with 18 features were classified as the proposed feature group. Details are described in the following feature selection and results part. In the last stage of diagnosis process, the selected features with labels were combined and input to five classifiers while the ensemble of bagged tree is the proposed algorithm for classification. Five classifiers with five feature combinations respectively were evaluated in term of accuracy, specificity, sensitivity and AUC.

The framework consists of 4 major steps: delineation of ROIs, feature extraction, feature selection, and classification. Each of the steps are described in details in the following parts of this paper.

**Delineation of ROIs**

To improve the accuracy of the diagnosis method, precisely segmentation of the ROIs from irrelevant parts was essential for feature extraction. Thus, GGO region, which is the main CT manifestations, was taken as ROI. The software of MIRcro 1.4 was used to extract the rectangle ROI of COVID-19 and GP. ROIs were delineated in CT images based on aforementioned GGOs. The main processes of ROI delineation are as follows: 1) A rectangular region as large as possible, which is the ROI, was delineated within GGOs and export the whole image with delineation to a PNG image; 2) PNG images were binarized to get the ROI boundary and fill the rectangular region to get the ROI template; 3) The ROI templates were used to extract the ROI in the original DICOM image; 4) The gray level of the ROI image was converted to 256 gray levels and the images were resized to 32×32 pixels. Consequently, 615 COVID-19 and 146 GP ROIs were cropped. It is apparent that COVID-19 images were four times larger than GP images while imbalanced data cannot reflect the true distribution of two categories, which could affect the classification performance. Thus, we rotated the GP images by 90, 180, 270 degrees. Ultimately, the number of GP images were augmented to 584. In conclusion, 1199 ROI images were enrolled for feature extraction.

**Feature extraction**

In this stage, a total of 34 statistical texture features were extracted from the ROIs images of COVID-19 and GP as shown in table 4, which contains 13 GLCM features, 15 GLGCM features and 6 histogram features. GLCM and GLGCM are the predominant second-order statistical texture analysis methods to characterize the features of an image, which have been widely applied in medical image processing. Besides, GLCM considers the statistical and spatial relationship of the pixels in the image. It is created by calculating how often pairs of pixel with specific values and in a specified spatial relationship occur in an image [5]. Then 13 statistical texture features are extracted based on the grey level co-occurrence matrix. In contrast with GLCM, GLGCM captures not only gray scale features but also the second order statistics of gray level gradients while gradients indicate the information of image edge.
which provides significant features of an image [6]. In addition, the histological characteristics of COVID-19 and GP can be well reflected in the gray mode, and the gray histogram is an intuitive statistical method 27. It is a one-dimensional function of the gray level and belongs to the first-order statistical method. After obtaining all texture feature data, due to the different calculation methods of each feature, the numerical value changes in a wide range. Therefore, to facilitate calculation, all data are normalized to [0, 1] based on their respective dimensions, the normalized equation (1) is as follows: (see Equation 1 in the Supplemental Files)

$$X^* = \frac{X - \text{MIN}}{\text{MAX} - \text{MIN}}$$

Where $X$ is the original data of the $N_{th}$ dimension, MIN is the minimum value in the $N_{th}$ dimension, MAX is the maximum value in the $N_{th}$ dimension, $X^*$ is the normalized feature.

| Feature groups | Description |
|----------------|-------------|
| GLGCM          | 1. Little gradient advantage; 2. Large gradient advantage; 3. Gray heterogeneity; 4. Gradient heterogeneity; 5. Energy; 6. Average gray; 7. Average gradient; 8. Gray mean square error; 9. Gradient mean square error; 10. Correlation; 11. Gray entropy; 12. Gradient entropy; 13. Hybrid entropy; 14. Inertia; 15. Inverse difference moment; |
| GLCM           | 16. Angular second moment; 17. Correlation; 18. Entropy; 19. Contrast; 20. Inverse difference moment; 21. Sum average; 22. Sum entropy; 23. Sum variance; 24. Variance; 25. Dissimilarity; 26. Inertia; 27. Difference variance; 28. Difference entropy; |
| Histogram      | 29. Entropy; 30. Uniformity; 31. Mean intensity; 32. Standard deviation; 33. Kurtosis; 34. Skewness |

**Feature selection**

Feature selection plays a critical role in enhancing the performance of medical imaging classification. High dimensional features causes over-fitting, lower accuracy, comprehension difficulty and it is rather time-consuming. Thus, feature selection is leveraged to select a subset of features, which makes the evaluation criteria reach the optimal level, from the original feature set. ReliefF algorithm is classified as a typical filter method for feature selection 28. It calculates the weight for each feature based on the capability to identify feature value differences between nearest neighbor instance pairs. The weight of a random given feature decreases if the difference of the feature value is observed in the nearby instance of the same class (called nearest hit) . Alternatively, the weight of a random given feature increases if the difference of the feature value is observed in the nearby instance of the difference class (called nearest miss) . ReliefF searches for k nearest hits and misses and averages their contribution to the weights of each feature 29. Furthermore, m random features will be selected and repeat the algorithm for n times to improve reliability. After n iterations, divide the sum of each feature's weights by n. This is noted as the relevance. Features with relevance greater than a threshold T are selected. Therefore different thresholds yielded different combinations. Generally, T is supposed to be greater than 0, for negative weights means negative impact on classification.
Feature Classification

The ensemble of bagged tree, which is a supervised classification scheme, is regarded as the proposed classification algorithm. It adopts the idea of bootstrap aggregating to enhance the stability and increase the accuracy. The training data is partitioned into several subsets by random selecting with replacement. Each subset is trained to construct independent base models. All the prediction from different models are applied to majority voting scheme. As a result, it reduces the influence of noise data and is less susceptible to over-fitting, which improves the robustness.

For comparison with the performance of the EBT algorithm, SVM, LR, DT, KNN are implemented with the same texture feature extraction methods and the same feature selection method. To superiorly identify the differences of the results, a 10-fold cross-validation strategy method is adopted. In 10-fold cross-validation, the original data set is equally divided into 10 subsamples. Of the 10 subsamples, 9 subsamples are used as training set while the remaining one is taken as validation set. The process is repeated 10 times until each of the 10 subsamples is utilized as validation set. The average of the 10 results is retained as the final estimation.

Statistics

The classification metrics used included AUC, sensitivity, specificity, accuracy. Let TP (true positive) denotes the number of samples belonging to class positive and correctly classified; FN (false negative) denotes the number of samples belonging to class negative but misclassified; FP (false positive) denotes the number of samples not belonging to class positive but misclassified as class positive; FN (false negative) denotes the number of samples not belonging to class negative but misclassified as class negative. Classification accuracies are reported in terms of accuracy, sensitivity, specificity as: (see Equations 2-4 in the Supplementary Files)

Abbreviations

CT: Computed Tomography; COVID-19: novel coronavirus pneumonia; GP: general pneumonia; EBT: ensemble of bagged tree; DICOM: digital imaging and communications in medicine; kV: kilovolt; GLCM: gray level co-occurrence matrix; GLGCM: gray level-gradient co-occurrence matrix; SVM: support vector machine; LR: logistic regression; DT: decision tree; KNN: K-nearest neighbor with Minkowski distance equal weight; ROC: receiver operating characteristic curve; AUC: the receiver operating characteristic curve; TP: true positive; FN: false negative; FP: false positive; FN :false negative.

Declarations

Acknowledgements

We would like to acknowledge the funding agencies for the support of the work. The content is solely the responsibility of the authors and does not necessarily represent the official views of Ruian Science and
Authors’ contributions

CL and XW are equally contributed as the first authors. Corresponding Author: WP. CL, XW, and WP accomplished the manuscript writing, data analysis, and machine learning model developing. CL and QS accomplished data collecting, clinical expertise providing, and manuscript revising. All authors read and approved the final manuscript.

Funding

This work was supported by the funding of Ruian Science and Technology Bureau (MS2020023, MS2020025).

Availability of data and materials

The dataset analyzed during the current study was derived from the following public domain resources: https://pan.baidu.com/s/1Ux9dpa1wtquNee4hEh1OWQ, code: k23c.

Ethics approval and consent to participate

The Institutional Review Board of Ruian People’s Hospital, Ruian city, Zhejiang province of China approved the retrospective study (YJ202014), and the requirement for written informed consent was waived.

Consent for publication

All authors consent for the publication of this manuscript.

Competing interests

The authors declare that they have no competing interests.

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**Figures**

![Figure 1](image.png)

**Figure 1**

Samples of COVID-19 and GP CT images Picture A is the CT image of COVID-19 with bilateral GGOs while picture B is the CT image of GP with unilateral GGO. The red arrows point at the GGOs of COVID-19 and the blue arrow points at the GGO of GP.
Figure 2

the weight curves of 34 features based on ReliefF algorithm. The X axis represents the numbers of features. The Y axis represents the weights of different features at different times. The algorithm run 1000 times represented by curves with different colors. The bold line represents weight = 0.11, which is the proposed threshold T.

Figure 3

Accuracy comparison of five classifiers with different feature combinations
Figure 4
Sensitivity comparison of five classifiers with different feature combinations

Figure 5
Specificity comparison of five classifiers with different feature combinations
Figure 6

Comparison of receiver operating characteristic curves for the proposed classifier, KNN, SVM, LR, and DT using feature combination 5. The receiver operating characteristic curves for the proposed EBT models had an AUC that was significantly greater than that for four other models.
the flowchart of the proposed diagnosis framework. The framework consists of 4 major steps: delineation of ROIs, feature extraction, feature selection, and classification. Each of the steps are described in details in the following parts of this paper.

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