Abstract: The lung cancer reduces the breathing ability and it causes due to uncontrollable cells in the lungs. The fusion of Computed Tomography (CT) and Positron Emission Tomography (PET) has clear information about lungs comparing with individual CT and PET images. The fused image helps to find cancer in a starting stage. In this study, a novel method for fusion of CT and PET lung images using Wavelet Transform (WT) and MaxMin (MM) rule is presented. Initially, the CT and PET lung images are decomposed by WT. The subband coefficients of WT are extracted by using entropy features. Then MM rule is applied, after that the image is reconstructed to form the fused lung image. The performance is evaluated by Reference Image Database to Evaluate therapy Response (RIDER) lung database. Results and discussion shows the performance of Lung Image Fusion (LIF).

Keywords: Lung Image Fusion, Wavelet Transform, Maxmin Rule, RIDER Database.

I. INTRODUCTION

LIF based on structural similarity index and max rule is discussed in [1]. Initially, the CT and PET images are divided into different blocks. The CT block corresponds to the PET block. Then structural similarity index is applied to form the fused lung image. The thresholding technique is used to detect the lung nodule. Wavelet denoising and image fusion based ribs segmentation is discussed in [2]. The lung parenchyma was extracted by using Otsu method. Then the lung fusion is made by wavelet image fusion algorithm. The multiscale wavelet is applied for noise removal. The Gaussian mask is used for the segmentation and smoothened the ribs.

Lung fusion based on lung vessel registration is discussed in [3] using CT and magnetic resonance images. The perfusion analysis and lung vessel segmentation is performed for both images. The pixel intensity is adjusted, the feature point is also determined, and then finally the elastic matching is made to form a fused image. Lung fusion based on three-dimensional Convolutional Neural Network (CNN) is described in [4]. CNN is used for the LIF. The hu unit is used for the segmentation of lung images.

CT and PET LIF based on supervised co-segmentation is described in [5]. The input lung image features are extracted by using computational complexity. The cost for mono-modality, global cost function, cost for inconsistency and iterative optimization is used for lung image segmentation. Dual tree complex wavelet transform based PET-CT LIF is discussed in [6]. At first, the pretreatment and registration is used for the preprocessing technique, the higher and lower frequency components of dual-tree complex wavelet transform is used to form the fused image. The image reconstruction is also made. Finally, the fused image is obtained. Multistage fusion approach based on non-small cell lung cancer is discussed in [7]. The input CT and PET images are fused by using fuzzy clustering means, the ensemble clustering methods and fusion.

CNN based feature fusion and lung disease classification is described in [8]. The lung images are preprocessed at first. The LIF is made by using CNN and Gabor filters with enhanced information. Lung tumor classification based on multi layer perceptron is discussed in [9]. Initially, the lung nodules are segmented by gray level co-occurrence matrix. The features like homogeneity, mean, standard deviation, angular second moment, energy and standard deviation are extracted. The classification is made by multilayer perceptron and k-nearest neighbor. Lung cancer detection in CT lung images is discussed in [10]. Initially, the lung images are preprocessed by using image preprocessing and median filter. The region of interest is extracted by using morphological operations. Then the features are extracted by geometrical features. Support vector machine classifier is used for classification.

A novel method for CT and PET LIF using wavelet transform and maxmin rule is discussed in this study. The organization of the paper is as follows: Section 2 describes the methods and materials used for CT and PET LIF. In section 3 the results and discussion of lung fusion is described. The last section concludes the CT and PET LIF.

II. METHODS AND MATERIALS

LIF using CT and PET lung images based on WT and MM is shown in figure 1. Initially the lung images are decomposed by WT and it produces the subband coefficients. Then the entropy features are extracted. Finally, MM rule is applied to perform the LIF.

A. WT Decomposition

The different merit function in WT and fourier transform is similar to each other. WT uses the fourier and real space. WT is also used in object recognition [11], brain image classification [12] and weld image classification [13]. It returns the data vector with the same input length. WT decomposes into a set of wavelets which has the orthogonal of scaling and translations. The decomposition of WT has the compression of the wavelet spectrum in some data points. It is defined by,

\[ K(u,v) = \int_{-\infty}^{\infty} k(g)h^*(u,v)(g) dg \]  \hspace{1cm} (1)

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where $\xi$ is some function and $*$ is the conjugate symbol. The certain rules are performed under this function. In this study, the WT is used to decompose the CT and PET lung images and it produces the subband coefficients.

$$WET = -\sum_j G_j \log_2(G_j)$$  \hspace{1cm} (2)

where $G_j$ is the probability $j$ is the level of probability and the subband information is denoted as $-\log_2$. In this study, the WT coefficients are extracted by using entropy features.

C. MM Rule

It is the essential tool for decomposition in fuzzy logic rules and wavelet analysis. MM rule is frequently used in the lower and higher frequency components. The subproblem finds the min unit for the two class subproblem which is presented in the basic units. The min unit finds the minimum value for given inputs and max units finds the maximum value for the inputs. The two class subproblem for MM rule is defined by,

$$S_{a,b}^u = MIN\left(\begin{array}{c}S_{a,b}^u,\ldots,S_{a,b}^{K_u}\end{array}\right)$$  \hspace{1cm} (3)

$$S_{a,b} = MAX\left(\begin{array}{c}S_{a,b}^{1},S_{a,b}^{2},\ldots,S_{a,b}^{K_u}\end{array}\right)$$  \hspace{1cm} (4)

Where $u=1,2,\ldots,S_a$ and $S_{a,b}^{u}\ (u=1,2,\ldots, K_u, b=1,2,\ldots, S_a)$ is the base classifier output. In this study, MM rule is used for the CT and PET LIF. If PET value is less than CT apply min rule otherwise apply max rule. Then reconstruct the image to form the fused image.

III. RESULTS AND DISCUSSION

The LIF performance is evaluated by using RIDER database [17-18]. Some sample lung CT and PET images in RIDER database are shown in figure 2.

**Fig. 2. Sample lung images in the RIDER database**

At first, the input CT and PET lung images are given to WT and it produces lower and higher frequency subband coefficients. These subband coefficients are extracted by entropy features. Then the MM rule is applied for the fusion of CT and PET lung images. If WETCT is greater than WETPET apply min rule otherwise apply max rule. Then the inverse transform is applied to reconstruct the image. Finally fused mage is obtained by using WT and MM rule. Figure 3 shows the fused image obtained by using WT and MM rule.

**Fig. 3. Performance of fusion using WT and MM rule**

The performance of LIF is measured by Peak Signal to Noise Ratio (PSNR) values. The PSNR is measured by mean square error. The PSNR is measured by

$$\text{PSNR} = 10\log_{10}\left(\frac{P^2}{L}\right)$$  \hspace{1cm} (5)

where $P$ is the maximum function of input, and $L$ is a mean square error. Table 1 shows the performance of PSNR values for LIF using some sample images in the RIDER database.
### Table II: Performance of PSNR values for LIF

| Sample Images | PSNR Performance |
|---------------|------------------|
| S.No.         | CT (dB)           | PET (dB)         |
| 1             | 61.43             | 31.24            |
| 2             | 64.79             | 41.53            |
| 3             | 62.70             | 38.79            |
| 4             | 58.61             | 35.54            |
| 5             | 64.38             | 40.80            |

From Table I it is observed that the performance of PSNR is approximately 64.79 dB for CT images and 41.53 dB for PET images. It gives the best fusion performance by using WT and MM rule.

### IV. CONCLUSION

A novel method for LIF using WT and MM rule is presented in this paper. The input lung images are decomposed by WT to produce lower and higher frequency subband coefficients. These subband coefficients are extracted by entropy features and given to MM rule. If CT image value is greater than PET image value the min rule is applied otherwise max rule is applied. The inverse transform is applied to reconstruct the image and forms the LIF. Finally, the CT, PET and fused lung image is measured by using PSNR values for better performance using WT and MM rule.

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