Optical coherence tomography characteristics of in-stent restenosis are different between first and second generation drug eluting stents

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Aims: Characterization of neointimal tissue is essential to understand the pathophysiology of in-stent restenosis (ISR) after drug eluting stent (DES) implantation. Using optical coherence tomography (OCT), we compared the morphologic characteristics of ISR between first and second generation DES.

Methods and Results: OCT was performed in 66 DES-ISR, defined as >50% angiographic diameter stenosis within the stented segment. Patients with ISR of first generation sirolimus-eluting stents (SES), paclitaxel eluting stents (PES) and second generation zotarolimus-eluting stents (ZES), everolimus-eluting stents (EES) and biolimus-eluting stents (BES) were enrolled. Quantitative and qualitative ISR tissue analysis was performed at 1-mm intervals along the entire stent, and categorised as homogeneous, heterogeneous and neo-atherosclerosis. The presence of microvessels and peri-strut low intensity area (PSLIA) was determined in all ISR. Neoatherosclerosis was identified by lipid, calcium and thin-cap fibro-atheroma (TCFA) like lesions. We compared the two DES generations at both early (<1 year) and late (>1 year) follow-ups.

In second generation DES a heterogeneous pattern was prevalent both before and after 1 year (57.1% and 58.6% respectively). Neo-atherosclerosis was more common in the early period in first generation DES (19.4% vs 11.7%, p < 0.01), but after one year was more prevalent in second generation DES (7.0% vs 19.3%, p < 0.01). Similar prevalence of TCFA was observed in both groups in all comparisons.

Conclusions: When ISR restenosis occurs in second generation DES, the current data suggest a different time course and different morphological characteristics from first generation. Future prospective studies should evaluate the relationship between ISR morphology, time course and clinical events.

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1. Introduction

Although a significant reduction in the rate of in-stent restenosis (ISR) has been observed with first and second generation (G1 and G2) drug eluting stents (DES) compared with bare metal stents (BMS), this event still limits long term outcomes after percutaneous coronary intervention (PCI) (1,2). However, the basis for this observation is not yet fully understood. Optical coherence tomography (OCT) is the preferred modality to study arterial healing after stent implantation. Due to its high resolution, OCT can disclose plaque morphology with a sensitivity close to histology and provide an accurate assessment of stent deployment, with special focus on the number and distribution of covered struts (3,4). Recently, OCT has been used for the characterization of ISR and different tissue patterns have been described (5,6). Studies of DES-ISR are limited but there is an evidence that neointimal hyperplasia after DES may be more heterogeneous and occur earlier than the fibrotic intimal hyperplasia observed after BMS implantation (7,8). Furthermore, there is a histological evidence of neatherosclerotic tissue growth, mainly described within first generation DES-ISR, which is characterized by lipid and/or calcium deposition, macrophage infiltration and necrotic core formation. In some cases these lesions are almost indistinguishable from thin-cap-fibro-atheroma (TCFA) lesions found in native plaques (8,9) which are consistently shown to correlate with...
accrete coronary events (10–12), G2 DES, probably because of greater biocompatibility, have drastically reduced restenosis and stent thrombosis when compared with G1 DES (13–16). However, ISR has also been described with these new generation devices.

The aim of this study was to compare the morphologic characteristics of neo-intimal tissue in a consecutive series of ISR of G1 and G2 DES studied with OCT.

2. Methods

2.1. Study design and population

All consecutive patients with one or more ISR in a G1 or G2 DES, studied with OCT between January 2007 and December 2012, were considered for the study. ISR was defined as angiographically documented diameter stenosis greater than 50% within the stented segment. The region of interest extended from the distal to the proximal stent edge, excluding the margins. As in previous pathologic ISR studies (8), we considered overlapping and consecutive stents as one lesion, while stents separated by more than 5 mm were considered as separate lesions. Patients included in our study underwent coronary angiography as clinically indicated, due to stable angina or NSTE-acute coronary syndromes, or as elective scheduled angiographic follow-up (because of the type of lesion previously treated [left main or equivalent] or as part of approved DES trials) (17,18). The use of intravascular imaging with IVUS or OCT is routinely practised in our centre to diversify the treatment of ISR based on its prevalent mechanism (underexpansion vs hyperproliferation) as indicated and explained in the informed consent approved by the institutional review board. We excluded patients with total occlusion, ST-segment elevation myocardial infarction, cardiogenic shock, serum creatinine > 2 mg/dl and bare metal stent ISR.

2.2. Quantitative coronary angiography

Quantitative coronary angiography (QCA) was performed offline by a skilled analyzer blinded to patients’ clinical characteristics and OCT analysis, using dedicated cardiovascular measurement software (QAngio XA 7.1 Medis Medical Imaging System, Leiden, The Netherlands) on a single, selected 2D end-diastolic image frame. Care was taken to select projections and frames with minimal foreshortening and vessel overlap, analyzing the view that revealed the highest degree of stenosis. After careful calibration, lesion length, proximal and distal references, minimal luminal diameter (MLD) and percent diameter stenosis (%DS) were calculated. Based on QCA results, lesions were classified as focal restenosis: < 10 mm in length, or diffuse restenosis: > 10 mm in length (19).

2.3. Optical coherence tomography imaging and analysis

The OCT images were acquired, using a non-occlusive technique, through a 2.7 Fr C7 Dragonfly Imaging Catheter (LightLab Imaging Inc., Westford, MA, USA), flushed with undiluted contrast dye and calibrated before the acquisition, which was inserted distal to the lesion of interest. A mechanical pullback at a speed of 20 mm/s was started during continuous automatic flushing of 2–5 ml/s of iodixanol (Visipaque™ 320 mg I/ml GE Healthcare, Amersham, UK) to ensure blood clearance from the coronary arteries, using a Medrad injector (Medrad Inc., Warrendale, PA, USA).

Quantitative and qualitative OCT analyses were performed off-line by agreement of two experienced analysts, blinded to clinical and angiographic lesion characteristics using commercial software (LightLab; St. Jude, Minneapolis, MN, USA), at every 1 mm cross section (CS) throughout the pullback from the distal to the proximal stent edge. Quantitative measurements included lumen and stent cross-sectional areas (CSA) (automatically traced and manually adjusted when required), neointimal hyperplasia (NIH) area (stent area–lumen area), percentage of NIH area (NIH area / stent area × 100) (Fig. 1) (20). For this analysis, only CSs with a percentage of NIH area ≥ 50% have been considered as effective part of the restenotic segment within stent (20).

Owing to a lack of consensus regarding the classification of ISR optical patterns and their histopathological basis, we analysed every evaluable cross section and adopted previously reported qualitative criteria for this analysis (6,9) (Fig. 2): 1) homogenous neointima; 2) heterogeneous neointima; and 3) neo-atherosclerosis. The homogenous pattern consists of tissue with uniform optical properties and no focal variation in backscattering. Heterogeneous tissue was identified by the presence of several variations in the optical backscattering properties and sub-classified in: layered pattern, consisting in concentric layers with different optical properties (thick adluminal high scattering layer and an abluminal low scattering layer), patchy pattern, irregular and highly echo-lucent regions throughout the layers, and speckled pattern, restenotic tissue with heterogeneous speckled bands (6,21). We defined neo-atherosclerosis as ISR showing optical areas consistent with at least one of the following features: lipids, diffusely bordered, signal-poor regions; calcium as well-delineated, low back-scattering heterogeneous regions; and thin-cap fibro-atheroma (TCFA) plaques, with a fibrous cap thickness ≤ 65 μm and an angle of lipid tissue ≥ 180 showing relevant signal attenuation (3,22). In these neo-atherosclerotic lesions, we also identified the presence of macrophages, multiple strong back reflections, resulting in a relatively high OCT signal variance within the fibrous cap (23). Hence, in the presence of the well defined neo-atherosclerotic features reported above, we classified the ISR as neo-atherosclerosis, while we defined the heterogeneous group as those with an OCT optical pattern which was neither homogeneous nor neoatherosclerotic tissue.

Furthermore, in all lesions we identified the presence of: microvessels, low backscattering structure with a diameter < 200 μm; peri-strut low intensity area (PSLIA) defined as a region around stent struts with homogenous lower intensity than surrounding tissue, without signal attenuation (24); malapposed struts, when the axial distance from DES strut to the luminal surface was longer than the strut/polymer thickness (25), excluding bifurcations; and uncovered struts. NIH thickness equal to 0 μm (26).

The decision to perform a dilatation before proceeding to OCT acquisition was left to the operator’s discretion on the basis of the angiographic findings. In the event of a tight ISR lesion, pre-dilatation with a 2.0 semi-compliant balloon, inflated at nominal pressure was allowed. Since balloon inflation may create a rupture of the fibrous cap, we excluded from our analysis disrupted intima like lesions and the presence of intraluminal material.

2.4. Statistical analysis

Categorical variables are expressed as numbers (percentages) and comparisons between groups were performed with χ² or Fisher’s exact test. Continuous variables are expressed as the mean ± standard deviation and compared with Independent T-test. The primary analysis compared ISR characteristics at early follow-up (less than 1 year) and late follow-up (more than 1 year) within the first or the second generation groups. Next, the comparison was performed between generations, within the early or late period (20). A p value < 0.05 was considered statistically significant. All statistical analyses were performed using the SPSS software (SPSS Inc. Version 20, Chicago, Illinois).

2.5. Results

A total of 66 ISR lesions were identified in 41 consecutive patients enrolled in this study. We found 44 ISR within G1 DES: 21 sirolimus-eluting stents (SES) (Cypher SELECT, Cordis, Miami Lakes, FL, USA) and 23 paclitaxel-eluting stents (PES) (Taxus EXPRESS and Liberté, Boston Scientific, Natick, MA, USA). We also identified 22 ISR lesions in G2 DES: of which 11 everolimus-eluting stents (EES) (9 Xience, Abbott Vascular, Santa Clara, CA, USA; and 2 Promus, Boston Scientific,
Fig. 1. Quantitative optical coherence tomography analysis. Representation of measured areas. CSA: cross sectional area; NIH: neointimal hyperplasia.

Lumen CSA

NIH CSA = Stent CSA - Lumen CSA

% NIH CSA = NIH CSA / stent CSA ×100

Fig. 2. Qualitative optical coherence tomography analysis. For definitions, refer in the text. 1) Homogeneous pattern of ISR. 2) Heterogeneous patterns subsequently subdivided in three subtypes: 2a) layered pattern; 2b) patchy pattern; and 2c) speckled pattern. 3) Neo-atherosclerosis and its main features: 3a) lipid plaque; 3b) calcium deposit; 3c) thin-cap fibroatheroma; and 3d) detail of macrophage presence in a lipid plaque. 4) Miscellaneous ISR characteristics: 4a) microvessels; 4b) peri-strut low intensity areas; 4c) overlapping stents; and 4d) malapposed struts.
2.6. Clinical characteristic

Baseline patients' clinical characteristics are shown in Table 1. There were no major differences between groups with the exception of a higher prevalence of previous myocardial infarction within G2 group in those with longer follow-up compared with patients with shorter follow-up (p = 0.04). More often the left circumflex was the culprit artery in the early follow-up of G1 compared with G2 DES (p = 0.04). The rate of use of ACE-inhibitors differed among groups.

2.7. QCA analysis

QCA analyses are summarised in Table 2. Within G1 DES focal restenosis predominated, whereas in G2 ISR a diffuse pattern was prevalent before 1 year with focal ISR more frequent at later time points (p = 0.02).

Quantitative analyses did not differ between early and late ISR of G1 DES. In the G2 group, the earlier lesions were significantly longer and with lower mean MLD and MIA, as well as higher %DS (p < 0.01).

The stent types within each DES generation were similar. Time from stent implantation to the index coronary angiography was not different on the evaluation of vascular healing after stent deployment using quantitative and qualitative OCT assessment, depicts a different pattern of ISR between G1 and G2 DES. We compared the two generations at two separate time points, before and after 1 year. Furthermore we analysed the differences of ISR pattern within each generation overtime.

2.8. OCT analysis

The quantitative analysis showed similar lesion length among groups. We found different mean absolute values of stent CSA and NIH CSA between generations and that the percentage of NIH CSA was lower for G2 DES both in the early and the late period (p < 0.01) (Table 3).

The qualitative analysis performed in the entire stent is reported in Table 4 and Fig. 4. A homogeneous pattern predominated in both early and late G1 DES-ISR, increasing overtime, while the heterogeneous and neoatherosclerotic lesions were less prevalent in the early phase and became even more infrequent at later time points (p < 0.01 in all comparisons). In G2 DES, we found a heterogeneous pattern more frequently at both early and late time points. The homogeneous pattern tended to become less prevalent overtime, while the frequency of neoatherosclerotic lesions tended to increase (p < 0.01 in all comparisons).

TCFAs as well as macrophages were rare and their prevalence did not differ between generations and overtime. Microvessels were more common in the early period in G1 ISR, but then decreased in prevalence; PSLIA was less common in G1 but more prevalent in G2 DES (p < 0.01). We found similar prevalence of overlapping and malapposed CSs in our analysis, however a significant increase in the number of uncovered struts was found associated with G1 ISR overtime.

3. Discussion

ISR is still the main reason of PCI failure and its predictors seem to be largely the same across the spectrum of BMS, G1 and G2 DES (27). Despite shared trigger factors, several data suggest a different composition of the restenotic tissue within different devices (7–9). Our study, focusing on the evaluation of vascular healing after stent deployment using quantitative and qualitative OCT assessment, depicts a different pattern of ISR between G1 and G2 DES. We compared the two generations at two separate time points, before and after 1 year. Furthermore we analysed the differences of ISR pattern within each generation overtime.

3.1. Comparison between first and second generation DES

We showed that ISR in G1 DES had mainly a homogeneous OCT pattern before and after one year, whereas in G2 DES the heterogeneous features were prevalent. In both generations the percentage of CSs with neo-atherosclerosis remained below 20% and the absolute prevalence was similar between generations. Similar prevalence of TCFAs appeared between generations.

ISR is thought to be a manifestation of abnormal vessel healing after stenting and provides the anatomic substrate for target lesion revascularization (TLR) and possibly acute coronary syndromes (7,28). Although there are few data on the histopathological basis of OCT-ISR patterns, the homogeneous type is thought to be the more common expression of the uncontrolled neointimal cell proliferation typical of BMS. The heterogeneous pattern, sometimes resembling neoatherosclerotic lesions, seems to be more frequent in later phases and in DES (22). Differences in the type of restenosis observed in different DES types have been previously reported (7–9). The underlying processes are likely multifactorial though the precise mechanisms remain unknown. Experimental evidence suggests that neo-atherosclerosis is associated with delayed arterial healing compounded by lethal injury to smooth muscle and endothelial cells (29). Therefore, the heterogeneous OCT images in DES may represent phenomena such as peri-strut inflammation. DES structure itself can influence vessel healing. Variables like different stent platforms, strut thickness, durability of the polymer, kinetics of drug release as well as post-deployment optimisation can explain differences observed in ISR observed in different DES platforms.

There is no consensus on the interpretation of different optical patterns and its histopathological basis. Previous studies demonstrated that restenotic tissue with speckled pattern exhibited myxomatous neointima tissue, containing extracellular matrix with proteoglycans (30,31). DES suppress the immunological response of the treated arterial wall. Therefore, delayed arterial healing, including replacement of extracellular matrix by smooth muscle cells or collagen, might contribute to this speckled image. The layered pattern may arise from a difference in smooth muscle cell density and orientation along the radial axis of ISR, with a more compact and concentric orientation in the inner luminal border, with reduced density and longitudinal orientation toward the vessel exterior. Alternatively the findings may be explained by the progressive attenuation of light travelling through the tissue (6). Conversely, neo-atherosclerosis, as reported in the "methods", is recognised according to well defined OCT features.

Many clinical studies have shown that G2 DES have superior efficacy and safety profile than G1 DES (13–15,17). We need to emphasize that the relationship between ISR morphology determined by OCT and clinical outcome is not established. In this study, only angiographically...
significant ISR was included, so our results may differ from the common healing process of the stent types reported or from less pronounced in- stent proliferation not enrolled in our registry. Moreover, we support the hypothesis that the dichotomous distinction in homogeneous and heterogeneous patterns does not have a clinical correlation by itself. No data exist about the risk of clinical events correlated with a layered, as heterogeneous patterns does not have a clinical correlation by itself. No

angiographic and QCA data, analysis per lesion.

Table 2

| Variable                        | First generation (n = 44) | p   | Second generation (n = 22) | p   | p*  | p** |
|---------------------------------|--------------------------|-----|---------------------------|-----|-----|-----|
|                                 | ≤ 1 year (n = 13)       | ≥ 1 year (n = 31) |               | ≤ 1 year (n = 14) | ≥ 1 year (n = 8) |       |       |
| Restenosis pattern              |                          |     |                          |     |     |     |
| Focal                           | 11 (84.6)                | 20 (64.5) | 0.28                     | 5 (35.7) | 7 (87.5) | 0.02 | 0.02 | 0.40 |
| Diffuse                         | 2 (15.4)                 | 11 (35.5) | 0.28                     | 9 (64.3) | 1 (12.5) | 0.02 | 0.03 | 0.40 |
| Lesion length, mm               | 7.7 ± 4.5                | 12.2 ± 8.8 | 0.09                     | 18.7 ± 14.4 | 7.5 ± 3.6 | 0.01 | 0.02 | 0.15 |
| RD, mm                          | 2.9 ± 0.6                | 3.0 ± 0.7 | 0.48                     | 3.0 ± 0.6 | 3.0 ± 0.8 | 0.89 | 0.65 | 0.98 |
| MLD, mm                         | 1.1 ± 0.6                | 1.0 ± 0.5 | 0.75                     | 0.8 ± 0.4 | 1.4 ± 0.5 | <0.01 | 0.12 | 0.07 |
| MLA, mm²                       | 1.2 ± 0.9                | 1.3 ± 1.9 | 0.80                     | 0.6 ± 0.5 | 1.6 ± 1.2 | <0.01 | 0.06 | 0.05 |
| Diameter stenosis, %            | 64.0 ± 16.2              | 67.0 ± 15.7 | 0.63                     | 71.7 ± 16.2 | 54.4 ± 7.1 | <0.01 | 0.22 | <0.01 |
| Stent type                      | Cypher                   | 5 (38.5) | 16 (51.6) | 0.52 | – | – | 0.09 | NA | NA |
|                                | Taxus                    | 8 (61.5) | 15 (48.4) | – | – | – | – | – |
|                                | Xience                   | – | – | 3 (21.4) | 6 (75.0) | – | – | – |
|                                | Promus                   | – | – | 2 (14.3) | 0 (0.0) | – | – | – |
|                                | Resolute                 | – | – | 8 (57.1) | 2 (25) | – | – | – |
|                                | BioMatrix                | – | 1 (7.1) | 0 (0.0) | – | – | – | – |
|                                | Time from previous stent to ISR | 10.0 ± 2.8 | 37.0 ± 18.3 | <0.01 | 8.1 ± 3.1 | 13.8 ± 4.0 | <0.01 | 0.12 | <0.01 |

Continuous variables are expressed as the mean ± SD; categorical variables as number (%). ISR: in-stent restenosis; MLA: minimal lumen area; MLD: minimal lumen diameter; QCA: quantitative coronary analysis. RD: reference diameter; p: comparison within each DES generation; p*: comparison of early ISR between generations; p**: comparison of late ISR between generations.
with previous papers reporting malapposed and uncovered struts in DES after OCT follow-up (25,26). This finding supports the concept of heterogeneity of vascular healing response after stenting, with possible co-existence of hyperplastic tissue and uncovered struts in adjacent segment (35,36), possibly due to uneven distribution of polymer and loading drug eluted, and overlapping and different deployment results in each CS.

The quantitative lesion analysis performed by both QCA and OCT showed less severe features within G2 DES, conceptually in line with the lower incidence of restenosis and TLR coming from clinical studies (13–16).

3.2. Comparison overtime within generations

This study, missing serial OCT analysis of the target restenotic lesions, does not claim to represent a reliable report of ISR pattern evolution overtime. Hence the interpretation of ISR pattern changes, based on an indirect comparison of OCT findings coming from lesions with a different follow-up, is performed aware of this limitation and is only hypothesis generating.

We found that in G1 DES the homogeneous pattern was prevalent before 1 year and even more represented afterwards. On the contrary the other patterns seemed to decrease. The heterogeneous pattern had higher prevalence in G2 both before and after 1 year, with the same absolute percentage, while neo-atherosclerosis was significantly more prevalent in the second period.

Several pathological studies confirmed that neoatherosclerotic features can be found in some restenotic lesions, often related to the time post-stent implantation (32,37). Habara et al. observed neoatherosclerotic restenosis more frequently within DES than BMS (31% vs 16%; p < 0.001). In the former group neoatherosclerosis appeared to manifest earlier (420 days vs. 2160 days respectively, p < 0.001) (9). Available data suggest a trend toward more rapid neoatherosclerotic changes in SES, although the frequency of neo-atherosclerosis in both PES and SES was higher than that in BMS (8). The heterogeneous pattern, as well as neo-atherosclerosis, could represent delayed healing within the stented segment, correlated to individual response to each stent platform. As discussed above, this apparently more sustained inflammation within G2 DES cannot be assumed as a general rule in their healing response, neither can be directly correlated to a worse prognosis.

The mean follow-up was 29 months for G1 and 11 for G2 DES. Even if sufficient to show neo-atherosclerosis changes within DES (9), we cannot exclude that a longer time course would be needed to unmask further differences in optical ISR between groups (22). Although in BMS some authors showed that in the long term the probability of neoatherosclerotic changes rises, the same hypothesis cannot be directly applied to DES. In these devices the neoatherosclerotic phenomenon seems to start earlier but no data exist about the evolution overtime. Our data shows, at least in G1 DES, a lower prevalence of heterogeneous and neoatherosclerotic patterns in the late follow-up.

In G1 DES PSLIA prevalence decreased, whereas the opposite happened in G2 ISR, probably revealing a sustained peri-strut inflammation process. Teramoto et al. reported that PSLIA was more frequently observed with DES than BMS and that these regions were hypocellular regions, suggesting the presence of fibrinoid or proteoglycans as a consequence of delayed arterial healing (38). Their role in the possible progression of neo-atherosclerosis needs further investigation.

3.3. Limitations

The discussion has already focused on some limitations of the study, correlated to the nature of the registry enrolling selected patients with angiographically significant ISR, and the lack of serial OCT analysis. Furthermore, we want to underline that OCT has intrinsic limitations in the qualitative analysis of restenotic tissue and the differentiation of some patterns was sometimes difficult. OCT findings were not confirmed by

### Table 3
Quantitative OCT analysis per cross-section with ISR > 50%.

| Variable                  | First generation (n = 1036) | p   | Second generation (n = 641) | p   | p*  | p**  |
|---------------------------|-----------------------------|-----|-----------------------------|-----|-----|-----|
|                           | ≤ 1 year (n = 309)          |     |                            |     |     |     |
| Mean stent CSA, mm²       | 5.0 ± 2.1                   | 0.88| 8.4 ± 3.2                   | 0.01| <0.01| 0.01|
| Mean lumen CSA, mm²       | 1.6 ± 1.3                   | 0.86| 1.9 ± 0.5                   | 0.01| <0.01| 0.08|
| NIH CSA, mm²              | 3.5 ± 1.0                   | 0.91| 2.4 ± 0.7                   | 0.01| <0.01| <0.01|
| NIH area, %               | 72.1 ± 12.1                 | 0.79| 61.1 ± 8.4                  | 0.01| <0.01| <0.01|
| Restenosis length, mm     | 71.7 ± 11.9                 | 0.62| 6.4 ± 6.4                   | 0.50| 0.86| 0.88|
|                           | >1 year (n = 727)           |     |                            |     |     |     |
| Mean stent CSA, mm²       | 5.1 ± 1.7                   | 0.88| 4.3 ± 1.1                   |     |     |     |
| Mean lumen CSA, mm²       | 1.6 ± 1.2                   | 0.86| 1.9 ± 0.5                   |     |     |     |
| NIH CSA, mm²              | 3.5 ± 0.9                   | 0.91| 2.4 ± 0.7                   |     |     |     |
| NIH area, %               | 71.4 ± 14.9                 | 0.79| 55.5 ± 5.2                  |     |     |     |
| Restenosis length, mm     | 53.6 ± 6.7                  | 0.62| 4.7 ± 2.5                   |     |     |     |

Continuous variables are expressed as the mean ± SD. CSA: cross sectional area; NIH: neo-intimal hyperplasia. p: comparison within each DES generation; p*: comparison of early ISR between generations; p**: comparison of late ISR between generations.
histopathological analysis and come from observations in a relatively small number of patients.

4. Conclusions

When ISR restenosis occurs in second generation DES, the current data suggest a different time course and different morphological characteristics from first generation. Future prospective studies should evaluate the relationship between ISR morphology, time course and clinical events.

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