Imaging Alzheimer’s disease pathophysiology with PET

Lucas Porcello Schilling1,2,3, Eduardo R. Zimmer1,2,3,4, Monica Shin1,2, Antoine Leuzy1,2,5, Tharick A. Pascoa1,2, Andréa L. Benedet1,2, Wyllians Vendramini Borelli3, André Palmini3, Serge Gauthier2, Pedro Rosa-Neto1,2

ABSTRACT. Alzheimer’s disease (AD) has been reconceptualised as a dynamic pathophysiological process characterized by preclinical, mild cognitive impairment (MCI), and dementia stages. Positron emission tomography (PET) associated with various molecular imaging agents reveals numerous aspects of dementia pathophysiology, such as brain amyloidosis, tau accumulation, neuroreceptor changes, metabolism abnormalities and neuroinflammation in dementia patients. In the context of a growing shift toward presymptomatic early diagnosis and disease-modifying interventions, PET molecular imaging agents provide an unprecedented means of quantifying the AD pathophysiological process, monitoring disease progression, ascertaining whether therapies engage their respective brain molecular targets, as well as quantifying pharmacological responses. In the present study, we highlight the most important contributions of PET in describing brain molecular abnormalities in AD.

Key words: Alzheimer’s disease, positron emission tomography, amyloid imaging, neuroinflammation, neurodegeneration, tau.

INTRODUCTION

Alzheimer’s disease (AD) was first described in 1906, when the German psychiatrist Alois Alzheimer reported the clinical and pathological features from a patient called Auguste Deter. At age 51, she became afflicted by an obscure progressive neuropsychiatric condition characterized by severe cognitive decline associated with behavioral symptoms. Five years after admission, she became mute and confined to her bed. Similarly to many patients, her death came as a consequence of septicemia. At the necropsy, the brain histopathological examination revealed the presence of amyloid plaques and neurofibrillary tangles, both of which later became known...
as the neuropathological hallmarks of AD. The term “Alzheimer’s disease” was introduced by the psychiatrist Emil Kraepelin in 1910, in his Handbook of Psychiatry. Initially considered a rare disease, AD became recognized as a frequent condition in aging individuals as well as the leading cause of dementia.

The neuropathological features of AD constitute the extracellular deposition of amyloid-β (Aβ) aggregates (senile plaques), intracellular inclusions of hyperphosphorylated tau aggregates (neurofibrillary tangles; NFTs), brain atrophy and cell depletion. These features silently accumulate and propagate across brain regions for many years, leading to subsequent clinical and functional decline. At the clinical stage of symptoms of dementia, these pathophysiological processes have already significantly compromised a large proportion of brain circuits involved in cognition. In its typical presentation, AD is characterized by progressive cognitive impairment initially confined to the episodic memory system.

The research criteria for the diagnosis of AD were first defined in 1984 by a working group jointly established by the National Institute of Neurological and Communicative Disorders and Stroke (NINCDS) and the Alzheimer’s Disease and Related Disorders Association (ADRDA). The NINCDS-ADRDA criteria assumed a static association between the pathological and clinical characteristics of AD. These criteria were useful and widely adopted, remaining in use for over 25 years. During the last decade, important advances in genetics, biochemistry, clinical, and pathological characterization of dementias have taken place, including the development of in vivo biomarkers of AD pathophysiology, leading to changes in the criteria for AD. An International Working Group (IWG) initiated these revisions, followed by the National Institute on Aging and Alzheimer’s Association workgroup (NIA-AA), leading to new diagnostic criteria including predementia stages of AD. In particular, the NIA-AA research criteria encompasses asymptomatic “preclinical” AD, mild cognitive impairment (MCI) due to AD, and AD dementia stages.

This disease framework incorporates important advances such as the notion of clinical and pathophysiological progression, the genetic form of AD, as well as atypical presentations of AD. Importantly, AD pathophysiology now assumes a progressive cascade of events associated with Aβ toxicity, which triggers a series of downstream biochemical cascades including tau hyperphosphorylation, synaptic depletion, neuroinflammation, and abnormal neurotransmission.

PET biomarkers for amyloid deposition

Though the pathogenesis of AD remains unclear, the hallmark of this neurodegenerative disease is the deposition of Aβ plaques, together with other features, such as the presence of NFTs. Aβ deposits are known to progressively accumulate in certain brain regions over the course of the disease, beginning long before the clinical onset. The canonical PET molecular agent capable of detecting fibrillary Aβ in vivo is the carbon-11 labelled thioflavin T derivative 2-(4'-methylaminophenyl)-6-hydroxybenzothiazole, also known as [11C]Pittsburgh Compound-B ([11C]PbB). The most widely studied amyloid PET tracer, [11C]PbB is considered the benchmark for PET-amyloid imaging. The short half-life of carbon-11 (20 minutes), however, limits its use to centers possessing an on-site cyclotron and specialized radiochemistry. The new generation of amyloid ligands, labeled with fluorine-18, have a longer half-life of approximately 110 minutes. Due to these differences in half-life, these fluorine-18 labeled compounds can be regularly produced at a cyclotron site and distributed to other facilities.

Previous studies indicate that patients with MCI present 20-30% higher prevalence of amyloid positivity when compared to controls, which suggests that both amnestic and nonamnestic MCI are associated with an increased risk for AD. This association is much more relevant in the amnestic MCI subtype, but it is important to highlight that a large number of MCI patients are amyloid negative, supporting the theory that MCI is not always due to amyloid-related AD pathology. A positive amyloid-PET scan increases the probability of conversion to AD, however, the interval over which MCI amyloid positive patients may convert to AD dementia is variable, ranging from 1 to 5 years. It is important to keep in mind the present limited clinical utility of detection of...
AD pathophysiology in MCI patients, given the lack of efficacious therapy as well as the ethical limitations when proposing amyloid imaging in patients meeting clinical criteria for MCI. On the other hand, positive amyloid-PET scans in MCI patients provides confirmation that this clinical situation occurs due to AD pathophysiology, supporting the idea of investing in non-pharmacological interventions, such as cognitive enrichment and diet and lifestyle changes. By contrast, a negative amyloid-PET scan in patients presenting cognitive impairment suggests other non-AD pathologies, such as frontotemporal lobar degeneration, hippocampal sclerosis, or argyrophilic grain disease. Although Parkinson’s disease (PD) and dementia with Lewy bodies (DLB) are neurodegenerative disorders associated with brain deposition of fibrillary aggregates of α-synuclein protein, individuals with these synucleinopathies and cognitive decline have shown variability with regard to the presence of an abnormal amyloid-PET scan.28,29 Interestingly, individuals presenting with Parkinson’s disease (PD) dementia have shown lower brain amyloid burden than AD, dementia with Lewy bodies, exhibiting similar burden to controls. On the other hand, patients presenting dementia with DLB have shown higher amyloid burden than controls, comparable to levels seen in AD patients.30,31 Interestingly, these studies have suggested that a positive amyloid-PET scan in DLB individuals might be associated with more rapid clinical progression.28,30

Table 1. Summary of amyloid imaging agents currently available for quantifying brain amyloid.

| Alternative name     | Parent molecule | Amyloid affinity (Ki, nM) | Plasma metabolites | Typical injected dose (MBq) | Typical imaging time (min) |
|----------------------|-----------------|---------------------------|--------------------|-----------------------------|-----------------------------|
| [11C]PIB             |Research Use     | 0.9                       | Polar              | 250–450                     | 40–90                       |
| [18F]Flutemetamol    | Vizamyl®        | 0.7                       | Polar              | 250–450                     | 90–110                      |
| [18F]Florbetapir     | Amvid®          | 2.2                       | Polar and non-polar| 300                         | 50–70                       |
| [18F]Florbetaben     | Neuraceq®       | 2.4                       | Polar and non-polar| 300                         | 90–130                      |
| [18F]NAV4694         | BAY-94-9172, AV-1| 0.7                      | Polar              | 300                         | 50–60                       |

Appropriate Use Criteria (AUC) for clinical amyloid imaging, recommending that the use of amyloid imaging be limited to patients showing progressive and unexplained cognitive decline with uncertain diagnosis, early onset dementia and/or atypical clinical presentation, and when knowledge of amyloid status is expected to alter the therapeutic approach. Clinical utilities of amyloid imaging are restricted to specific cases. Patients with early-onset dementia (commonly defined as onset before 65 years of age) have a lower probability of AD pathophysiology underlying their cognitive decline than late-onset cases. In this regard, amyloid imaging might clarify whether underlying brain amyloidosis is associated with clinical syndromes such as primary progressive aphasia, dementias characterized by a predominance of executive dysfunction, visuospatial symptoms, progressive apraxia, and corticobasal syndrome. Given the economic and family impact of the diagnosis of AD in this population, an elevated level of diagnostic certainty is highly desirable. Furthermore, the presence of amyloid pathology might provide the rationale for proposing the clinical use of cholinesterase inhibitors in this population. The AIT contraindicates the use of amyloid imaging in asymptomatic people or in those with a cognitive complaint but no clinical confirmation of impairment, for determining the severity of dementia and for non-medical reasons, such as insurance, legal or employment decisions.

Finally, recently incorporated into AD research diagnostic criteria, amyloid PET plays a major role in defining AD. The IWG criteria classified amyloid PET as a useful biomarker which supports clinical diagnosis, especially when the presentation is atypical.33 Hence, amyloid PET has increasingly been used in clinical trials, particularly for enriching study populations comprising individuals with a high probability of presenting AD or for monitoring target engagement of anti-amyloid therapies. How-
However, one limitation of CSF Aβ42-PiB exhibits a high affinity and specificity for Aβ plaques, as opposed to Lewy bodies or tau proteins, showing high accuracy in the evaluation of Aβ plaque burden. In individuals with AD, [11C]PiB uptake is distributed in the frontal, medial and lateral posterior parietal cortices, precuneus, occipital cortex and lateral temporal cortices, as well as in the striatum (Figure 1). Low [11C]PiB uptake is typically observed in the cerebellar cortex.

A recent Cochrane review study on [11C]PiB for early diagnosis of AD in individuals with MCI estimated sensitivity of 96% (95% confidence interval: 87-99) and median specificity of 58%. A growing consensus emerging from longitudinal studies indicates that disease-modifying therapies targeting amyloid should be administered at very early stages of the disease. Concentrated efforts worldwide are focusing on advancing the diagnosis of AD to a preclinical stage. Elevated [11C]PiB binding in nondemented subjects indicates that it may be sensitive for the detection of preclinical AD, suggesting a 20 to 30-year interval between first amyloid positivity and onset of dementia.

Presently, [11C]PiB is one of the most accurate agents for localizing and quantifying Aβ deposition; however, the short half-life of carbon-11 restricts its use to facilities with an onsite cyclotron and expertise in carbon-11 radiochemistry. Hence, the overall production and utilization costs are not generally affordable. In order to solve this issue, recent studies have focused on fluorine-18 labeled radiopharmaceuticals, whose longer half-life allows for regional distribution and commercialization. Widely used as a biomarker in the diagnostic criteria for AD, cerebrospinal fluid (CSF) also confirms Aβ pathology, with CSF Aβ42 having an inverse correlation with [11C]PiB SUVR values. However, one limitation of CSF Aβ42 is that it does not provide any regionalized information on amyloid burden in the brain.

Fluorine-18 labeled ligands. While the short half-life of carbon labeled radiotracers limits the application of [11C]PiB in clinical practice, fluorine-18 labeled amyloid PET radiopharmaceuticals have been developed, with a growing potential for clinical and research purposes. These compounds provide a new window of opportunity in the assessment of preclinical and clinical AD due to the 110-minute half-life of fluorine-18, a massive difference in terms of distribution logistics when compared to [11C]PiB production. At present, four radiofluorinated labeled radiopharmaceuticals are drawing scientific attention: [18F]3-F-PiB ([18F]flutemetamol), [18F]AV-45 ([18F]florbetapir), [18F]AV-1 or [18F]BAY94-9172 ([18F]florbetaben), and [18F]AZD4694 or [18F]NAV4694.

Similarly to [11C]PiB, these fluorine-18 amyloid tracers exhibit significant binding to fibrillar Aβ in the brain, albeit with some differences. [18F]Flutemetamol, [18F]florbetapir, and [18F]florbetaben are less specific than [11C]PiB, displaying white matter binding whereas [18F]NAV4694 shows more specific grey-white matter demarcation and better pharmacokinetic properties as a potential competitor of [11C]PiB PET. The Food and Drug Administration (FDA) and European Medicines Agency (EMA) have already approved [18F]florbetapir (Amyvid™), [18F]flutemetamol (Vizamyl™), and [18F]florbetaben (Neuraceq™) for use in clinical practice, while [18F]NAV4694 is currently in phase III trials.

While holding great research potential, all four compounds discriminate healthy controls from AD subjects with high accuracy. [18F]Florbetapir has shown remarkable accuracy in amyloid detection, with clinical application even in preclinical AD. The diagnostic value of [18F]flutemetamol has been tested recently in symptom-
PET BIOMARKERS FOR NEUROINFLAMMATION

A factor known to be involved in the pathogenesis of AD is the immune response, with initial association between amyloid deposits and immune response emerging among elderly in their 70s and 80s. More recently, there is emerging knowledge on components of innate immunity associated with AD pathology, as well as increasing discussion over the beneficial and detrimental effects of the immune response in AD. Another controversial topic is the start point of neuro-inflammatory processes observed in AD brains, which raises the question as to whether inflammation is a cause or a consequence of AD pathology. Despite the initial assumption of their occurrence only in late stages of the disease, inflammatory changes in the CSF can be detected in MCI patients, revealing the possibility of involvement of the immune system at very early stages of AD.

In a bid to answer the as yet unsolved questions regarding the Janus face of inflammation in AD, PET imaging is being used in vivo to trace markers of neuroinflammation with promising outcomes, as outlined below.

Radiopharmaceuticals for imaging microglial activation. Neuroinflammatory changes are a part of AD pathology, and microglial activation in areas affected by neurodegeneration is a key brain tissue event. Microglial activation occurring in early stages of AD dementia is associated with a significant elevation in the fractional area of reactive microglia following the formation of neuritic plaques comprising fibrillar Aβ. Using a specific ligand for the 18-kDa translocator protein (TSPO), formerly called the peripheral benzodiazepine receptor (PBR), quantification of microglial activation in vivo has been measured. Probably due to its poor specific binding, initial [11C]PK11195 studies in AD showed negative results. However, improvements in the [11C]PK11195 tracer, particularly with the utilization of its dextro-isomer, the radiotracer [(R)-PK11195, revealed increased sensitivity for detecting TSPO expression in parieto-temporal, entorhinal, and cingulate cortices of AD patients. In [11C]PBI+ AD patients, high microglial activation has been observed, with an inverse correlation between cognition and microglial activity. However, a recent study reported that the inclusion of a vascular component results in an amplified signal in AD patients, suggesting that an increase in [11C]-(R)-PK11195 sensitivity signal modeling may be required.

Other TSPO radiopharmaceuticals have been designed aimed at improving pharmacokinetics and specificity. In this regard, preclinical studies involving radiotracers [(2)-FEDAA1106 or [11C]AC5216 have shown promising results in AD-like transgenic models, and [11C]DA1106 PET imaging showed greater binding in AD patients compared to healthy control subjects. Another recent clinical study using [(2)-FEDAA1106 — a novel TSPO ligand with in vitro affinity superior to that of [11C]DAA1106 — showed widespread increases in MCI patients when compared to healthy controls, with these values predicting the conversion to AD dementia stage within a 5-year follow-up period.

Although applications in studies of AD patients have not been performed, [11C]AC5216 has shown promising pharmacokinetic features and a higher affinity than [11C]PK11195 in healthy subjects. However, the potential clinical applications of TSPO radiotracers are limited by the rs6971 polymorphism in the TSPO gene, which confers lower uptake in polymorphism carriers (~30%) in comparison to non-carriers. Importantly, the cannabinoid receptor type 2 (CB2) was identified as a marker of microglial activation, leading to greater attention to the endocannabinoid system. In this respect, preclinical studies of CB2 using [11C]A-836339 showed upregulation in a transgenic model displaying cerebral amyloidosis.
PET BIOMARKERS OF NEURODEGENERATION

PET radiopharmaceuticals of tau pathology. Misfolding and aggregation of hyperphosphorylated tau deposition into NFTs has a key role in AD pathophysiology. It has been proposed that tau pathology propagates across brain circuits. NFTs have been associated with neuronal dysfunction, cell death, and cognitive impairment. CSF levels of total tau (t-tau) and phosphorylated tau (p-tau) have been associated with disease severity, with altered tau levels in the CSF being interpreted as surrogate markers of neurodegeneration in AD. Despite this evidence, the clinical application of CSF tau as an AD biomarker has been further discussed elsewhere.

CSF tau biomarkers are somewhat disadvantageous compared to imaging biomarkers given the need for a lumbar puncture. Moreover, CSF measurements provide global estimates of the disease process without any information regarding the topographic localization of NFT. Finally, the quantification of p-tau and t-tau protein varies significantly across centers. Due to these features, imaging methods for NFT quantification are extremely important, particularly for assessing upcoming tau-based therapeutics. Given this scenario, several radiotracers characterized by high affinity for tau fibrils and with suitable kinetics have been developed, including the benzothiazole derivative \(^{[1]}\text{C}\)PBB3, the phenylquinoline derivatives—\(^{[1]}\text{F}\)THK-523, \(^{[1]}\text{F}\)THK-5105, and \(^{[1]}\text{F}\)THK-5117—and benzimidazole pyrimidine derivatives, such as \(^{[1]}\text{F}\)T807 and \(^{[1]}\text{F}\)T808.

\(^{[1]}\text{C}\)PBB3 has shown to rapidly cross both the blood-brain barrier (BBB) and neuronal plasma membranes, binding to intraneuronal tau inclusions. In vitro and ex vivo autoradiographic studies have shown that \(^{[1]}\text{C}\)PBB3 produced specific, high-contrast labeling of neuronal tau inclusions in the brain stem of mice models expressing human tau pathological mutations. The same findings were reported with in vitro autoradiography and AD tissue, showing evident radiolabelling of fibrillar aggregates in specific regions of the hippocampus (including CA1), and the frontal cortex. Similarly, a clinical PET study using \(^{[1]}\text{C}\)PBB3 in probable AD patients revealed increased tracer binding in lateral temporal and frontal cortices, in line with the distribution of tau pathology at Braak stage V/VI, and with higher SUVRs correlating with lower memory scores. A slight increase in \(^{[1]}\text{C}\)PBB3 retention was also observed around the hippocampus of a control subject who showed decline on the Mini-Mental State Examination (MMSE), consistent with Braak stage III/IV or earlier.

Aside from \(^{[1]}\text{C}\)PBB3, the fluorinated probes \(^{[1]}\text{F}\)T-807 and \(^{[1]}\text{F}\)T-808 are also potential tau ligands. An autoradiography study using AD brain tissue has shown that \(^{[1]}\text{F}\)T-807 exhibits strong binding to NFTs, with a selectivity estimate of 29-fold for tau relative to Aβ. In addition, comparing double immunohistochemical staining of NFTs and Aβ on adjacent tissue sections, \(^{[1]}\text{F}\)T-807 autoradiography showed that tracer binding co-localized with immunoreactive NFTs, not with Aβ plaques. In the case of \(^{[1]}\text{F}\)T-808, it also has a high affinity and good selectivity for NFTs over Aβ, which was indexed by autoradiographic studies. In addition, \(^{[1]}\text{F}\)T-808 presents fast brain uptake followed by a rapid washout, suggesting low non-specific binding, which is consistent with in vivo findings obtained using \(^{[1]}\text{F}\)T-807. Moreover, the first human brain using \(^{[1]}\text{F}\)T-807 showed elevated SUVR in AD compared to MCI and healthy control subjects. Distinct patterns of tracer accumulation, in line with Braak staging, was observed across the frontal, temporal and parietal cortices, as well as in the hippocampus/entorhinal region.

Another class of fluorinated probes includes the THKs, which have exhibited high affinity and selectivity for tau aggregates. In vitro preliminary studies have reported \(^{[1]}\text{F}\)THK-523 binding affinity for tau fibrils, with subsequent autoradiographic analysis using AD medial temporal brain sections showing accumulation of \(^{[1]}\text{F}\)THK-523 in the pre- and pri-α layers of the entorhinal cortex and hippocampal CA1 region. Immunohistochemistry confirmed that these findings were consistent with the density of PHF-tau deposition. Subsequently, histofluorescence and autoradiographic studies revealed that \(^{[1]}\text{F}\)THK-523 binding to NFTs co-localized with tau immunoreactivity, with no visible binding to Aβ plaques. However, recent immunohistochemical and histofluorescence studies questioned \(^{[1]}\text{F}\)THK-523’s future in both research and clinical settings due to very high non-specific white matter binding. Moreover, preliminary clinical data have suggested that \(^{[1]}\text{F}\)THK-523 does not bind tau inclusions in non-AD tauopathies.
The second generation of THKs was developed, which includes $^{18}$F]THK-5105 and $^{18}$F]THK-5117. Binding studies conducted in vitro using $^{11}$C]PIB and $^{18}$F]THK-5105 and $^{18}$F]THK-5117 have found increased binding affinity to synthetic truncated tau (K18ΔK280) fibrils—comprising the four repeat regions (244-372) in the absence of lysine 280 (ΔK280)—with both tracers proving superior to $^{18}$F]THK-523. The selective binding capacity of these compounds was further examined using in vitro autoradiography and AD mesial temporal brain sections, showing increased accumulation of the radiotracer with particularly high binding in the Sommer’s sector of the hippocampus, the parahippocampus, and the subiculum. These findings were confirmed through staining and immunohistochemistry, with reduced binding among healthy controls. Additional assessment of $^{18}$F]THK-5105, conducted using $^{11}$C]PIB and AD hemibrain sections, observed dense accumulation of $^{18}$F]THK-5105 in tau-rich areas—including the hippocampus/para-hippocampus, insula, cingulate gyrus and inferior and middle temporal gyri—with the pattern of tracer binding corresponding to the recognized distribution of tau pathology but not to that of Aβ or areas showing elevated retention of $^{11}$C]PIB. In addition, further studies of biodistribution conducted in normal mice showed diffuse and rapid brain uptake and fast clearance, with the kinetics of both tracers superior to those reported for $^{18}$F]THK-523.

$^{18}$F]FDG Radiotracer. The glucose analogue 2-deoxy-2-(F)luoro-D-glucose ($^{18}$F]FDG) PET has been utilized to assess cerebral glucose metabolism. $^{18}$F]FDG images have been interpreted as markers of neuronal activity and synaptic density. The typical AD metabolic signature consists of hypometabolism in the parieto-temporal association, medial temporal, posterior cingulate and frontal cortices, with relative preservation of the visual cortex, primary sensory motor cortices, basal ganglia, thalamus, and cerebellum (Figure 2). This hypometabolic signature is frequently observed in AD patients and in over 85% of pathologically-confirmed cases. However, in atypical focal cortical syndromes of AD, topographic variants of hypometabolism have been identified. For example, compared to typical AD, patients with logopenic primary progressive aphasia presented with disproportionate left temporoparietal hypometabolism. Patients with posterior cortical atrophy showed hypometabolism predominantly in occipito-parietal regions; some patients can present hypometabolism in the frontal eye fields. Patients with early onset AD also show greater metabolic reductions, with hypometabolism from mild dementia comparable to that observed in late onset cases with severe dementia. These findings are supported by studies showing more aggressive progression from patients with early onset AD and, possibly, by the cognitive reserve theory.

In amnestic MCI (aMCI) patients, the pattern of hypometabolic changes usually occurs in brain regions classically affected in AD, but to a lesser degree. The patterns of brain metabolism in aMCI and non-amnestic MCI (naMCI) subjects are similar, however, aMCI has shown a decrease in medial temporal lobe metabolism and naMCI hypometabolism in the right prefrontal region. Some authors report that the anterior hippocampal formation can contribute to differentiating MCI patients from healthy control subjects, although other data refutes this, with the partial volume effect in the metabolism of the hippocampal formation on $^{18}$F]FDG imaging constituting a complicating factor. The posterior cingulate is the most relevant area for predicting conversion from MCI to AD, given that hippocampal hypometabolism is highly influenced by the atrophy observed on MRI and, after correcting...
for the partial volume effect, this finding is no longer supported.\textsuperscript{117} \textsuperscript{[18F]}FDG has limited clinical value in MCI patients due to the lack of specificity for AD pathophysiology. At a population level, however, subjects with MCI presenting a more marked or ‘AD-like’ pattern have been found to convert to dementia at higher rates,\textsuperscript{126,127} with accuracies in the range of 75 to 100%.\textsuperscript{128,129} The magnitude of hypometabolism in the parietal and posterior cingulate cortices in MCI is associated with memory decline.\textsuperscript{130,131} As compared to decliners, stable MCI populations tend to exhibit hypometabolism restricted to the dorsolateral frontal cortex.\textsuperscript{132,133}

In order to study the progression to MCI and AD among cognitively normal older individuals, \textsuperscript{[18F]}FDG-PET has been used to predict cognitive decline with an accuracy approaching 80%).\textsuperscript{131,135} Progressive reductions in PET glucose metabolism were observed years before the appearance of clinical symptoms, with reductions in the hippocampus preceding declines in cortical regions\textsuperscript{134} in a clinicopathological study that evaluated cognitively normal individuals followed through MCI to pathologically-confirmed AD. The same metabolic changes have been noted in cognitively normal subjects homozygous for a susceptibility gene, the apolipoprotein E (APOE) \epsilon 4 allele,\textsuperscript{130,133} asymptomatic carriers of genetic mutations associated with early onset familial AD,\textsuperscript{128,129,136} and those with a maternal family history of AD, as compared to those with a paternal history or no family history of AD.\textsuperscript{137} Ultimately, \textsuperscript{[18F]}FDG will potentially prove of use in the characterization of a subgroup of patients exhibiting neurodegeneration in the absence of Aβ deposition.\textsuperscript{138,139} These patients, classified in the category of “suspected non-amyloid pathophysiology (SNAP)”, could suggest that the onset of neurodegeneration in AD may not depend on the accumulation of Aβ.\textsuperscript{140}

**IMAGING ALZHEIMER’S DISEASE PATHOPHYSIOLOGY IN EXPERIMENTAL MODELS**

A miniaturized version of PET, termed microPET, has made non-invasive imaging of small animals possible, such as rats and mice. In addition, advances in genetic engineering have led to the development of diverse animal models harboring human pathological gene mutations, which are capable of mimicking amyloid and tau pathologies (for review see (141)). These models show progressive deposition of amyloid or tau, in parallel with significant cognitive decline, and are highly suited to longitudinal assessment with microPET.

To date, several studies have investigated AD pathophysiological events in rodent models with microPET (for review see (142)). However, few such studies have been conducted using a longitudinal design. Recently, the first prolonged longitudinal study with microPET evaluating amyloid was published and revealed non-linear patterns of amyloid deposition during full disease progression.\textsuperscript{143} By contrast, to our knowledge, there are no longitudinal studies in the literature following tau pathology, and such studies are anxiously awaited by the AD community.\textsuperscript{144} In this context, longitudinal studies associating these animal models and microPET imaging have high translational capability, which indicates that data collected can be rapidly translated to clinical studies. In addition, microPET longitudinal studies offer unprecedented opportunities for monitoring the effectiveness of innovative therapeutic strategies.

**CONCLUSION**

Predictions based on biomarkers indicate that AD pathophysiological abnormalities precede the onset of clinical symptoms by at least two decades. By obtaining earlier AD diagnosis, it will be possible to develop potential innovative therapies that may impact the natural progression of AD. In fact, several clinical studies testing potential new drugs are currently underway with amyloid and tau being the most promising pharmacological targets (for review see (145)). In this scenario, PET radiotracers and neuropathological features for these processes are crucial to determine amyloid and tau engagement and to assess treatment response in clinical trials. In keeping with this, radiopharmaceuticals for neuroinflammatory molecular imaging can equally contribute to the development of potentially effective anti-inflammatory interventions. Although the majority of PET studies in AD populations have focused on Aβ imaging, several ‘non-amyloid’ radiopharmaceuticals exist for evaluating neurodegeneration, neuroinflammation and perturbations in neurotransmission across the spectrum of AD, potentially contributing to improved therapeutic perspectives for AD (for review see (146)).

At present, neurology is experiencing a new era which encompasses imaging assessment for patients suspected of having AD. Thus, it is extremely important to accurately establish those patients who are candidates for performing a cerebral PET exam (e.g. amyloid imaging). In the case of amyloid positivity, this biomarker-based information reflects an elevated risk for AD, and health professionals should exercise caution when ordering this test in non-demented patients (e.g. healthy subjects and MCI patients). In the coming few years, when more effective therapies are likely to become available, amyloid imaging will be increasingly applied to identify
patients with early AD or at risk of developing AD; preferably in association with \textsuperscript{18}FFDG imaging in order to combine pathological (amyloid deposition) and metabolic (hypometabolism) information. Other radiotracers will also play a key role for research in AD (Table 2), especially in targeting novel therapies and for monitoring the response and efficacy of new drugs (e.g. tau and neuroinflammation).

**Author contribution.** Lucas Porcello Schilling collected and critically analysed literature, contributed with tables and wrote the paper; Eduardo R. Zimmer collected and critically analysed literature, contributed with figures and wrote the paper; Monica Shin collected and critically analysed literature and wrote the paper. Antoine Leuzy collected and critically analysed literature, contributed with figures and wrote the paper; Tharick A. Pascoal collected and critically analysed literature and wrote the paper; Wyllians V. Borelli collected and critically analysed literature and wrote the paper. André Palmini collected and critically analysed literature and wrote the paper; Serge Gauthier collected and critically analysed literature and wrote the paper; Pedro Rosa Neto collected and critically analysed literature and wrote and reviewed the paper.

**REFERENCES**

1. Cipriani G, Dokiotti C, Picchi L, Bonuccelli U. Alzheimer and his disease: a brief history. Neurol Sci. 2011;32(2):275-9.
2. Dahm R. Alzheimer's discovery. Curr Biol. 2006;16(21):R906-10.
3. Brockmeyer R, Johnson E, Ziegler-Graham K, Arrighi HM. Forecasting the global burden of Alzheimer’s disease. Alzheimers Dement. 2007;3(3):186-91.
4. Duyckaerts C, Delatour B, Potier MC. Classification and basic pathology of Alzheimer disease. Acta Neuropathol. 2009;118(1):5-36.
5. McKhann G, Drachman D, Folstein M, Katzman R, Price D, Stadlan EM. Clinical diagnosis of Alzheimer’s disease: report of the NINCDS-ADRDA Work Group under the auspices of Department of Health and Human Services Task Force on Alzheimer’s Disease. Neurology. 1984;34(7):909-44.
6. Jack CR, Jr., Albert MS, Knopman DS, et al. Introduction to the recommendations from the National Institute on Aging-Alzheimer’s Association workgroups on diagnostic guidelines for Alzheimer’s disease. Alzheimers Dement. 2011;7(3):257-62.
7. Dubois B, Feldman HH, Jacova C, et al. Research criteria for the diagnosis of Alzheimer’s disease: revising the NINCDS-ADRDA criteria. Lancet Neurol. 2007;6(8):734-46.
8. Dubois B, Feldman HH, Jacova C, et al. Revising the definition of Alzheimer’s disease: a new lexicon. Lancet Neurol. 2010;9(11):1118-27.
9. Spertling RA, Aisen PS, Beckett LA, et al. Toward defining the preclinical stages of Alzheimer’s disease: recommendations from the National Institute on Aging-Alzheimer’s Association workgroups on diagnostic guidelines for Alzheimer’s disease. Alzheimers Dement 2011;7(3):280-92.
10. Albert MS, DeKosky ST, Dickson D, et al. The diagnosis of mild cognitive impairment due to Alzheimer’s disease: recommendations from the National Institute on Aging-Alzheimer’s Association workgroups on diagnostic guidelines for Alzheimer’s disease. Alzheimers Dement 2011;7(3):270-9.
11. McKhann GM, Knopman DS, Chertkov H, et al. The diagnosis of dementia due to Alzheimer’s disease: recommendations from the National Institute on Aging-Alzheimer’s Association workgroups on
diagnostic guidelines for Alzheimer's disease. Alzheimer's Dement 2011;7(3):263-9.
12. Jack CR, Jr., Kropman DS, Jagust WJ, et al. Hypothetical model of dynamic biomarkers of the Alzheimer's pathological cascade. Lancet Neurol 2010;9(9):119-28.
13. Jack CR, Jr., Kropman DS, Jagust WJ, et al. Tracking pathophysiological processes in Alzheimer's disease: an updated hypothetical model of dynamic biomarkers. Lancet Neurol 2013;12(2):207-16.
14. McGeer PL, McGeer EG. The amyloid cascade-inflammatory hypothesis of Alzheimer's disease: implications for therapy. Acta Neuropathol 2013;126(4):479-97.
15. Goversi S, Mura E, Preda S, et al. Dangerous Liaisons between Beta-Amyloid and Cholinergic Neurotransmission. Curr Pharm Des 2014;20(15):2525-38.
16. Klunk WE, Engler H, Nordberg A, et al. Imaging brain amyloid in Alzheimer's disease with Pittsburgh Compound-B. Ann Neurol 2004;55(3):306-19.
17. Kemppainen NM, Aalto S, Wilson IA, et al. PET amyloid ligand [11C]PiB uptake is increased in mild cognitive impairment. Neurology. 2007;69(18):1603-6.
18. Ikonomovic MD, Klunk WE, Abrahamson EM, et al. Post-mortem correlates of in vivo PiB-PET amyloid imaging in a typical case of Alzheimer's disease. Brain. 2008;131(Pt 6):1630-45.
19. Leuzy A, Zimmer ER, Heuring K, Rosa-Neto P, Gauthier S. Use of amyloid PET across the spectrum of Alzheimer's disease: clinical utility and associated ethical issues. Amyloid. 2014;21(2):143-8.
20. Leuzy A, Zimmer ER, Bhat V, Rosa-Neto P, Gauthier S. Imaging biomarkers for amyloid: a new generation of probes and what lies ahead. Int Psychogeriatr. 2014;26(5):703-7.
21. Oketo A, Kovuenen J, Edison P, et al. Conversion of amyloid positive and negative MCI to AD over 3 years: an 11C-PiB PET study. Neurology. 2009;73(1):754-60.
22. Pike KE, Savage G, Villenagi VL, et al. Beta-amyloid imaging and memory in non-demented individuals: evidence for preclinical Alzheimer's disease. Brain. 2007;130(Pt 11):2837-44.
23. Vanderbergh G, Van Laere K, Ianniou A, et al. 18F-flutemetamol amyloid imaging in Alzheimer disease and mild cognitive impairment: a phase 2 trial. Ann Neurol. 2010;68(1):1398-403.
24. Wolk DA, Price JC, Saxton JA, et al. Amyloid imaging in mild cognitive impairment subtypes. Ann Neurol. 2009;65(5):557-68.
25. Jansen WJ, Ossenkoppele R, Knol DL, et al. Prevalence of cerebral amyloid pathology in persons without dementia: a meta-analysis. JAMA. 2015;313(19):1924-38.
26. Nordberg A, Carter SF, Rinne J, et al. A European multicentre PET study of fibrillar amyloid in Alzheimer's disease. Eur J Nucl Med Mol Imaging. 2013;40(1):104-14.
27. Forsberg A, Engler H, Almkvist O, et al. PET imaging of amyloid deposition in patients with mild cognitive impairment. Neurol Aging. 2008;29(10):1456-60.
28. Czlonkowska A, Carter SF, Reitz CD, et al. Imaging amyloid deposition in Lewy body diseases. Neurology. 2008;71(12):903-10.
29. Petrau M, Dzwana BA, Foerster BR, et al. Amyloid deposition in Parkinson's disease and cognitive impairment: a systematic review. Mov Disord. 2015;30(7):928-35.
30. Edson P, Rowe CC, Rinne JO, et al. Amyloid load in Parkinson's disease dementia and Lewy body dementia measured with [11C]PiB positron emission tomography. J Neurol Neurosurg Psychiatry. 2008;79(12):1331-8.
31. Claassen DO, Rowe VJ, Peller PJ, Petersen RC, Josephs KA. Amyloid and glucose imaging in dementia with Lewy bodies and multiple systems atrophy. Parkinsonism Relat Disord. 2011;17(3):160-5.
32. Johnson KA, Minoshima S, Bohnen NI, et al. Appropriate use criteria for amyloid PET: a report of the Amyloid Imaging Task Force, the Society of Nuclear Medicine and Molecular Imaging, and the Alzheimer's Association. J Nucl Med. 2013;54(3):476-90.
33. Dubois B, Feldman HH, Jacova C, et al. Advancing research diagnostic criteria for Alzheimer's disease: the IWG-2 criteria. Lancet Neurol. 2014;13(6):514-29.
34. Soucy JP, Bartha R, Bocti C, et al. Clinical applications of neuroimaging in patients with Alzheimer's disease: a review from the Fourth Canadian Consensus Conference on the Diagnosis and Treatment of Dementia 2012. Alzheimers Res Ther. 2013;5(Suppl 1):S3.
Tracking neuroinflammation in Alzheimer’s disease: the role of positron emission tomography imaging. J Neuroinflammation. 2014;11:120.

61. McGeer EG, McGeer PL. Inflammatory processes in Alzheimer’s disease. Prog Neuropsychopharmacol Biol Psychiatry. 2003;27(3):741-9.

62. Vehmas AK, Kawas CH, Stewart WF, Troncoso JC. Immune reactive cells in senile plaques and cognitive decline in Alzheimer’s disease. Neurol Aging. 2003;2(4):321-31.

63. Akijamra H, Barger S, Barnum S, et al. Inflammation and Alzheimer’s disease. Neurol Aging. 2000;21(3):383-421.

64. Cagnin A, Brooks DJ, Kennedy AM, et al. In-vivo measurement of activated microglia in dementia. Lancet. 2001;358(9286):481-7.

65. Versijpt JJ, Dumont F, Van Laere KJ, et al. Assessment of neuroinflammation and microrna activation in Alzheimer’s disease with radiolabelled PK11195 and single photon emission computed tomography. A pilot study. Eur Neurol. 2003;50(1):39-47.

66. Papadopoulos V, Baraldi M, Gularte TR, et al. Translocator protein (18kDa): new nomenclature for the peripheral-type benzodiazepine receptor based on its structure and molecular function. Trends Pharmacol Sci. 2006;27(8):402-9.

67. Groom GN, Junck L, Foster NL, Frey KA, Kuhl DE. PET of peripheral benzodiazepine binding sites in the microgliosis of Alzheimer’s disease. J Neuroced. 1995;36(12):2207-10.

68. Edison P, Archer HA, Gerhard A, et al. Microglia, amyloid, and cognition in Alzheimer’s disease. An [11C](PK)11195-PET and [11C]PiB-PET study. Neurobiol Dis. 2008;32(3):412-9.

69. Tomasi G, Edison P, Bertolotto A, et al. Novel reference region model reveals increased microglial and reduced vascular binding of 11C-(R)-PK11195 in patients with Alzheimer’s disease. J Neuroced. 2008;49(8):1249-56.

70. Higuchi M. Visualization of brain amyloid and microglial activation in mouse models of Alzheimer’s disease. Curr Alzheimer Res. 2009; 6(2):137-43.

71. Maeda J, Zhang MR, Okauchi R, et al. In vivo positron emission tomographic imaging of glial responses to amyloid-beta and tau pathologies in mouse models of Alzheimer’s disease and related disorders. J Neurosci. 2011;31(12):4720-30.

72. Yasuno F, Otta M, Kosaka J, et al. Increased binding of peripheral benzodiazepine receptor in Alzheimer’s disease measured by positron emission tomography with [11C]DAA1106. Biol Psychiatry. 2008;64(10):385-41.

73. Wischik CM, Edwards PC, Lai RY, Roth M, Harrington CR. Selective inhibition of Alzheimer disease-like tau aggregation by phenothiazines. Proc Natl Acad Sci U S A. 1996;93(20):11213-8.

74. Yasuno F, Kosaka J, Otta M, et al. Increased binding of peripheral benzodiazepine receptor in mild cognitive impairment-dementia conversions measured by positron emission tomography with [(1)C](DAA1106). Psychiatry Research. 2012;203(1):67-74.

75. Miyoshi M, Ito H, Arakawa R, et al. Quantitative analysis of peripheral benzodiazepine receptor in the human brain using PET with [(1)C]-AC5216. J Neuroced. 2009;50(7):1095-101.

76. Yoder KK, Kho N, Reischler SL, Rim S, Shen L, Saykin AJ. Influence of 5216. J Nuclear Med. 2009;50(7):1095-101.

77. Yoder KK, Nho K, Risacher SL, Kim S, Shen L, Saykin AJ. Influence of 5216. J Nuclear Med. 2009;50(7):1095-101.

78. Yoder KK, Nho K, Risacher SL, Kim S, Shen L, Saykin AJ. Influence of 5216. J Nuclear Med. 2009;50(7):1095-101.

79. Yoder KK, Nho K, Risacher SL, Kim S, Shen L, Saykin AJ. Influence of 5216. J Nuclear Med. 2009;50(7):1095-101.

80. Johnson KA, Schultz A, Betensky RA, et al. Tau PET imaging in aging and early Alzheimer’s disease. Neurology. 2014;80(1):110-9.

81. Marquie M, Normandin MD, Vanderburg CR, et al. Validating novel tau positron emission tomography tracer F-18-AV-1451 (T807) on post-mortem brain tissue. Ann Neuroced. 2015;78(5):787-800.

82. Sokoloff L, Reivich M, Kennedy C, et al. The [(14)C]deoxyglucose method for the measurement of local cerebral glucose utilization: theory, procedure, and normal values in the conscious and anesthetized albino rat. J Neuromed. 1977;28(5):897-916.

83. Schilling et al. PET and AD pathophysiology

84. Spires-Jones TL, Stoothoff WH, de Calignon A, Jones PR, Hyman BT. Tau pathophysiology in neurodegeneration: a tangled issue. Trends Neuroced. 2009;32(3):150-9.

85. Iqbal K, Liu F, Gong CX, Alonso Adel C, Grundke-Iqbal I. Mechanisms of tau-induced neurodegeneration. Acta Neuroced.2009;118(1):S3-69.

86. de Calignon A, Polidoro M, Suarez-Calvet M, et al. Propagation of tau pathology in a model of early Alzheimer’s disease. Neurou. 2012;73(4):685-97.

87. Buerger K, Teipel SJ, Zinkowski R, et al. CSF tau protein phosphorylated at threonine 231 correlates with cognitive decline in MCI subjects. Neurology. 2002;59(4):627-9.

88. Augustinack JC, Schneider A, Mandelkow EM, Hyman BT. Specific tau phosphorylation sites correlate with severity of neuronal cytotoxicity in Alzheimer’s disease. Acta Neuroced. 2002;103(1):26-35.

89. Bienenk H, Hampel H. CSF markers for incipient Alzheimer’s disease. Lancet Nucl. 2003;2(10):605-13.

90. Zimmer ER, Leuzy A, Gauthier S, Rosa-Neto P. Developments in Tau PET Imaging. Can J Neurol Sci. 2014;41(5):547-53.
of Alzheimer’s disease. FDG-PET studies in MCI and AD. Eur J Nucl Med Mol Imaging. 2005;32(4):486-510.

108. Minoshima S, Giordani B, Berent S, Frey KA, Foster NL, Kuhl DE. Metabolic reduction in the posterior cingulate cortex in very early Alzheimer’s disease. Ann Neurol. 1997;42(1):85-94.

109. Scholl M, Damian A, Engler H. Fluorodeoxyglucose PET in neurology and Psychiatry. PET Clin. 2014;9(4):371-90.

110. Rabinovici GD, Jagust WJ, Furst AJ, et al. Abeta amyloid and glucose metabolism in three variants of primary progressive aphasia. Ann Neurol. 2008;64(4):388-401.

111. Nestor PJ, Carne D, Fryer TD, Clarke J, Hodges JR. The topography of metabolic deficits in posterior cortical atrophy (the visual variant of Alzheimer’s disease) with FDG-PET. J Neurol Neurosurg Psychiatry. 2003;74(11):1521-9.

112. Kim EJ, Cho SS, Jeong Y, et al. Glucose metabolism in early onset versus late onset Alzheimer’s disease: an SPM analysis of 120 patients. Brain 2005;128(Pt 8):1790-801.

113. Jacobs D, Sano M, Marler K, et al. Age at onset of Alzheimer’s disease: relation to pattern of cognitive dysfunction and rate of decline. Neurology. 1994;44(7):1215-20.

114. Katzman R, Brown T, Thal LJ, et al. Comparison of rate of annual change of mental status score in four independent studies of patients with Alzheimer's disease. Ann Neurol. 1988;24(3):384-9.

115. Mosconi L, Blys M, Glodzik-Sobanska L, De Santi S, Ruskine H, de Leon MJ. Early detection of Alzheimer’s disease using neuroimaging. Exp Gerontol. 2007;42(1-2):129-38.

116. Nestor PJ, Fryer TD, Smielewski P, Hodges JR. Limbic hypometabolism in Alzheimer’s disease and mild cognitive impairment. Ann Neurol. 2003;54(3):343-51.

117. De Santi S, de Leon MJ, Ruskine H, et al. Hippocampal formation glucose metabolism and volume losses in MCI and AD. Neurobiol Aging. 2001;22(4):529-39.

118. Mosconi L, De Santi S, Li Y, et al. Visual rating of medial temporal lobe metabolism in mild cognitive impairment and Alzheimer’s disease using FDG-PET. Eur J Nucl Med Mol Imaging. 2006;33(2):210-21.

119. Cienci F, Del Sole A, Chiti A, et al. Differences in hippocampal metabolism between amnestic and non-amnestic MCI subjects: automated FDG-PET image analysis. The quarterly journal of nuclear medicine and molecular imaging : official publication of the Italian Assoc Nucl Med. 2009;53(6):646-57.

120. Coutinho AM, Porto FH, Duran FL, et al. Brain metabolism and cerebrospinal fluid biomarkers profile of non-amnestic mild cognitive impairment in comparison to amnestic mild cognitive impairment and normal older subjects. Alzheimers Res Ther. 2015;7(1):58.

121. Mosconi L, De Santi S, Li J, et al. Hippocampal hypometabolism predicts cognitive decline from normal aging. Neurobiol Aging. 2008;29(5):676-92.

122. Mosconi L, Tsui WH, De Santi S, et al. Reduced hippocampal metabolism in MCI and AD: automated FDG-PET image analysis. Neurology. 2005;65(1):1980-7.

123. de Leon MJ, Convit A, Wolf OT, et al. Prediction of cognitive decline in normal elderly subjects with 2-[(18)F]fluoro-2-deoxy-D-glucose/positron-emission tomography (FDG/PET). Proc Natl Acad Sci U S A. 2001;98(19):10966-71.

124. Samuraki M, Matsunari I, Chen WP, et al. Partial volume effect-corrected FDG PET and gray matter volume loss in patients with mild Alzheimer’s disease. Eur J Nucl Med Mol Imag. 2007;34(10):1658-69.

125. Chetelat G, Desgranges B, Landeau B, et al. Direct voxel-based comparison between grey matter hypometabolism and atrophy in Alzheimer’s disease. Brain 2008;131(Pt 1):60-71.

126. Chetelat G, Desgranges B, de la Sayette V, Vlader F, Eustache F, Baron JC. Mild cognitive impairment: Can FDG-PET predict who is to rapidly convert to Alzheimer’s disease? Neurology. 2003;60(8):1374-7.

127. Mosconi L, Perani D, Sorbi S, et al. MCI conversion to dementia and the APOE genotype: a prediction study with FDG-PET. Neurology. 2004;63(12):2332-40.

128. Drzezga A, Lautenschlager N, Siebner H, et al. Cerebral metabolic changes accompanying conversion of mild cognitive impairment into Alzheimer’s disease: a PET follow-up study. Eur J Nucl Med Mol Imag. 2003;30(8):1104-13.

129. Herholz K, Nordberg A, Salmon E, et al. Impairment of neocortical metabolism predicts progression in Alzheimer’s disease. Dement Geriatr Cogn Disord. 1999;10(8):494-504.

130. Anchisi D, Borroni B, Franceschi M, et al. Heterogeneity of brain glucose metabolism in mild cognitive impairment and clinical progression to Alzheimer disease. Arch Neurol. 2005;62(11):1728-33.

131. Herholz K, Salmon E, Perani D, et al. Discrimination between Alzheimer dementia and controls by automated analysis of multicenter FDG PET. Neuroimage. 2002;17(1):302-16.

132. Rossi S, Cappa SF, Babloni C, et al. Prefrontal [correction of Premotor] cortex in long-term memory: an “interference” approach using magnetic stimulation. Nat Neurosci. 2001;4(9):948-52.

133. Desgranges B, Baron JC, Eustache F. The functional neuroanatomy of episodic memory: the role of the frontal lobes, the hippocampal formation, and other areas. Neuroimage. 1998;6(2):198-213.

134. Mosconi L, Mistur R, Switalski R, et al. FDG-PET changes in brain glucose metabolism from normal cognition to pathologically verified Alzheimer’s disease. Eur J Nucl Med Mol Imag. 2009;36(5):811-22.

135. Drzezga A, Grimm-T, Remischneider M, et al. Prediction of individual clinical outcome in MCI by means of genetic assessment and 18F-FDG PET. J Nucl Med. 2005;46(10):1625-32.

136. Bateman RJ, Xiong C, Benzinger TL, et al. Clinical and biomarker changes in dominantly inherited Alzheimer’s disease. New Engl J Med. 2012;367(9):795-804.

137. Mosconi L, Blys M, Switalski R, et al. Maternal family history of Alzheimer’s disease predisposes to reduced brain glucose metabolism. Proc Natl Acad Sci U S A. 2007;104(49):19067-72.

138. Jack CR, Jr., Knopman DS, Weigand SD, et al. An operational approach to National Institute on Aging-Alzheimer’s Association criteria for preclinical Alzheimer disease. Ann Neurol. 2012;71(8):765-75.

139. Knopman DS, Jack CR, Jr., Wiste HJ, et al. Short-term clinical outcomes for stages of NIA-AA preclinical Alzheimer disease. Neurology. 2012;78(20):1576-82.

140. Knopman DS, Jack CR, Jr., Wiste HJ, et al. Brain injury biomarkers are not dependent on beta-amyloid in normal elderly. Ann Neurol. 2013;73(4):472-80.

141. Gotz J, Ittner LM. Animal models of Alzheimer’s disease and frontotemporal dementia. Nat Rev Neurosci. 2008;9(7):532-44.

142. Zimmer ER, Parent MJ, Cuello AC, Gauthier S, Rosa-Neto P. MicroPET imaging and transgenic models: a blueprint for Alzheimer’s disease clinical research. Trends Neurosci. 2014;37(11):629-41.

143. Maier FC, Wehr HF, Schmid AM, et al. Longitudinal PET-MRI reveals beta-amyloid deposition and rCBF dynamics and connects vascular amyloidositis to quantitative loss of perfusion. Nat Med. 2014;20(12):1485-92.

144. Zimmer ER, Leuzy A, Bhat V, Gauthier S, Rosa-Neto P. In vivo tracking of tau pathology using positron emission tomography (PET) molecular imaging in small animals. Transl Neurodegener. 2014;3(1):6.

145. Cian X, Hamad B, Dias-Laica C, The Alzheimer disease market. Nat Rev Drug Discov. 2015;14(10):675-6.

146. Schilling LPL, Zimmer ER, Gauthier S, Rosa-Neto P. Nonamyloid PET biomarkers and Alzheimer’s disease : current and future perspectives. Future Neuro. 2014;9(8):597-613.