A novel method for genetic transformation of *C. albicans* using modified-hydroxyapatite nanoparticles as a plasmid DNA vehicle

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In modern biological research, genetic transformation is an important molecular biology technique with extensive applications. In this work, we describe a new method for the delivery of plasmid DNA (pDNA) into a yeast species, *Candida albicans*. This method is based on the use of novel arginine–glucose–PEG functionalized hydroxyapatite nanoparticles (M-HAp NPs) as a vehicle which delivers pDNA into *Candida albicans* with a high transformation efficiency of $10^6$ cfu μg$^{-1}$ of pDNA, without the need for preparation of competent cells. A four-fold higher transformation efficiency as compared to that of the electroporation method was obtained. This new method could provide exciting opportunities for the advancement of the applications of yeasts in the field of biotechnology.

Introduction

Yeast has been associated with humans for the preparation of bread, wine, beer, sake, etc., since ancient times and these processes are the basis of modern biotechnology.1,2 Recently, yeast species are being used as experimental models to study signal processes and to characterize molecular events associated with human mitochondrial and neurodegenerative diseases.3–5 To advance the use of yeasts in industries and research, modification of yeast strains by delivering nucleic acids into the cell is crucial.6,7 Several types of yeast species such as *Saccharomyces*, *Aspergillus*, *Rhizopus*, etc. are genetically engineered for the efficient production of various drugs, industrial enzymes, vaccines, and chemicals including insulin, human serum albumin, etc.8–9 Different chemicals like phenolics, isoprenoids, alkaloids and polyketides are also produced by engineered yeast.10 However, delivery of DNA into yeast is a major challenge due to the presence of a tough cell wall which is composed of mannose-containing proteins and glycans. Various approaches like lithium acetate (LiAc)-based methodologies, electroporation, gene gun transformation, protoplast transformation, etc., have been developed to deliver nucleic acids into yeast cells.11–16 However, these methods have limitations such as a low transformation efficiency and high toxicity and many of them need costly reagents or equipment. Hence, there is a need for the development of transformation methods which are more efficient, less toxic and reproducible.

Recently, nanotechnology based approaches have received much attention in the field of gene delivery due to factors such as high DNA loading capacity, high transformation efficiency and ease of delivery. Several nanoparticle based transformation methods have been developed for bacterial and eukaryotic cells.17–21 However, to our knowledge, there is only one report on nanoparticle based DNA delivery in yeasts which used oligoelectrolyte polymeric nanoscale carriers for the delivery of DNA into yeasts like *Saccharomyces cerevisiae*, *Hansenula polymorpha* and *Pichia pastoris*.22 Therefore, development of biocompatible nanomaterial based DNA delivery methods for the transformation of yeast cells needs to be actively explored.

Hydroxyapatite nanoparticles (HAp NPs) being biocompatible are good candidates for DNA delivery and have been explored as carriers in animal and plant cells.23–26 HAp also has advantages as it exhibits high affinity to nucleic acids and can be easily transported through cell membranes.27–29 In this work, we have synthesized arginine (R), glucose (G) and polyethylene glycol (PEG) functionalized thin-rod HAp NPs (referred to as M-HAp NPs) which form stable complexes with pDNA. Successful transformation of pDNA in *Candida albicans* was achieved using these HAp NPs as nanovehicles. This newly developed method exhibited four-fold increase in the transformation efficiency as compared to the electroporation technique. To the best of our knowledge, this is the first report on the transformation of *C. albicans* using HAp NPs with high efficiency and no toxicity.
Materials and methods

Chemicals

Orthophosphoric acid, dimethyl sulfoxide, acetyl acetone and ammonium hydroxide were procured from Merck India. Calcium chloride dihydrate, kanamycin and genetin were obtained from Himedia, India. Kanamycin and genetin resistance gene containing plasmids and agarose were purchased from Geneti, India.

Bacterial strain. Escherichia coli DH5α engineered with kanamycin and genetin resistance gene containing plasmids.

Yeast strains. For transformation studies Candida albicans 183 was purchased from MTCC Chandigarh. This strain was sensitive to the combination of kanamycin and genetin antibiotics.

Synthesis of modified-HAp NPs

Hydroxyapatite nanoparticles (HAp NPs) were synthesized using a modified sol–gel method developed in our laboratory. In brief, 2 M calcium chloride dissolved in DMSO was stirred for 30 min, followed by dropwise addition of orthophosphoric acid. The Ca : P atomic ratio was maintained at 1.67. This was followed by the addition of acetyl acetone as a stabilizing agent and stirred for 1 h. Liquid ammonia was used for adjusting the pH to 10 and stirring was continued until complete gelation. Subsequently, 0.1 wt% arginine (R), 0.3 wt% glucose (G) and 0.05 wt% polyethylene glycol (PEG) were added and stirred for 2 h to functionalize the HAp NPs. Thorough washing of the final product was carried out using ethanol, followed by dialysis (using a dialysis bag, Bangalore Genei 110) against de-ionized (DI) water for 12 h with frequent change of water for active removal of adsorbed ions. The dialyzed samples were dried at room temperature. Arginine–glucose–PEG modified HAp NPs are referred to as M-HAp NPs in following text.

Characterization

X-ray diffraction (XRD) studies of HAp and M-HAp NPs were carried out for phase identification using an X-ray diffractometer (Miniflex II Rigaku, Japan) with monochromatic Cu Kα radiation (λ = 1.5405 Å) and a scan range of 2θ = 20° to 80°. The functional groups present in the synthesized compounds were ascertained by Fourier transform infrared spectroscopy (FTIR) (8201 PC Shimadzu, Japan), over the 4000–450 cm⁻¹ region. The pellets for FTIR analysis were obtained by mixing 1 mg of the powdered sample with spectroscopic grade KBr (Merck). The particle shape and size of the M-HAp NPs were studied using a transmission electron microscope (TEM) (Phillips CM 200). NP solutions were sonicated for 15–20 min and a drop of the dispersion was put on a copper coated grid and air dried in vacuum desicators. Dried samples were examined under a TEM at SAIF IIT Bombay. The zeta potential of M-HAp NPs was determined with a zeta potential analyzer (Delsa Nano S, Beckman Coulter, USA) at room-temperature. The samples were prepared by diluting the NP suspension with DI water. HAp and M-HAp NPs were analyzed by X-ray photoelectron spectroscopy (XPS) (AXIS Supra, Kratos Analytical, UK, monochromatic Al Kα, 75 W). A survey spectrum from 0–1000 eV and high-resolution spectra for Ca 2p, O 1s, P 2p N 1s and C 1s were recorded.

Plasmid isolation

The plasmid was isolated from E. coli and C. albicans using a Qiagen plasmid isolation midi kit, following the protocol specified by the manufacturer (Qiagen plasmid midi kit). It was 10 Kb in size and contained kanamycin and genetin resistance genes. It is represented as pDNA in the following text.

Plasmid DNA binding efficiency

M-HAp NPs (1 mg mL⁻¹) were suspended in DI water, sonicated for 10 min and mixed with 100 ng pDNA at various M-HAp NP : pDNA ratios (0 : 1 (control), 10 : 1, 30 : 1, 50 : 1, 70 : 1, and 100 : 1). The suspensions were incubated at room temperature for 5 min, centrifuged at 22 000 × g for 3 min and the pellet obtained was suspended in 50 μL of Tris–EDTA buffer; the dissolved pellet is termed the M-HAp NP–pDNA complex. Unbound pDNA was quantified by measuring the optical density (OD) of the supernatant at 260 nm using a UV spectrometer (UV2450, Shimadzu, Japan), using the supernatant of the NPs without pDNA as a blank. The DNA binding efficiencies (B.Es) were determined using the equation:

\[
\% \text{ B.E.} = \left[ \frac{([\text{pDNA}]) - ([\text{pDNA}])}{([\text{pDNA}])} \right] \times 100,
\]

where % B.E = percent binding efficiency, [pDNA] = the optical density of the initial amount of pDNA added to the reaction mixture and [pDNA] = the optical density of the unbound pDNA remaining in the sample.

Each of the M-HAp NP–pDNA complexes (20 μL) was loaded on 0.8% agarose gel and was run using an electrophoresis apparatus at 80 mV for 1 h. It was stained with ethidium bromide for 10 min and the results were recorded using a gel imager (Life technologies, India).

Dynamic light scattering of R-G-HAp NPs and R-G-HAp NP–pDNA complexes

DLS studies of M-HAp NPs and M-HAp NP–pDNA complexes were carried out in minimal media (M.M), phosphate buffered saline of pH 7.0 (PBS) and Sabouraud dextrose broth (SB). Samples were sonicated using a probe sonicator for 15 min after dispersion in the respective medium (0.1 mg/3 mL). DLS studies were carried out immediately and again after 30 min of sonication using a DLS analyzer (Nano Plus Micromeritics).

Transformation of non-competent C. albicans cells

Candida albicans was chosen as a model yeast organism for transformation studies. This strain was kanamycin and genetin sensitive, whereas the selected plasmid of size 10 Kb contains kanamycin and genetin resistance genes. It was streaked on Sabouraud dextrose agar (SDA) plates and incubated at 37 °C for 48 hours. A single colony from the streaked plate was inoculated into 10 mL Sabouraud broth (SB) and incubated at 37 °C for 48 h. The cells (2 × 10⁶) were added to
20 mL SB after a prescribed time period and incubated at 37 °C in a shaking incubator for 6–8 h. The cells were subsequently centrifuged in two sets at 10 000 rpm, each set containing 6 tubes with 1 mL culture. The pellets were dissolved in 200 
µL M.M for the first set and in 200 µL of SB media for the second set. Afterwards, 20 µL M-HAp NP : pDNA of various ratios (0 : 1, 50 : 1, 70 : 1, 80 : 1, 90 : 1 and 100 : 1) was added and vortexed for 5 min. Subsequently, the cells were heat-shocked for 30–60 s at 47 °C, chilled on ice for 2 min, mixed with the respective 1 mL SB/M.M broth, and incubated at 37 °C for 1 h on a rotary shaker. 100 µL of the cell suspension was transferred onto kanamycin (100 µg mL⁻¹) and geneticin (G418) (150 µg mL⁻¹) containing SDA plates and incubated at 37 °C for 36–48 h. The colonies were counted and transformation efficiencies (T.Es) were calculated using the formula TE = number of colonies on the plate/concentration of pDNA present in 100 µL cell suspension (in µg). A similar protocol was followed to measure the T.E for HAp NP mediated transformation.

Electroporation
pDNA of 500 ng concentration was added to 200 µL electrocompetent cells, mixed properly and transferred into an ice cold 1 mm-electroporation cuvette. The cuvette was placed in an electroporator which was set to 2.5 kV; 150 Ω; 22 µF module and press pulsed followed by the addition of 1 mL of SB/M.M media and incubated at 37 °C on a shaking incubator for 1 h. Subsequently, 100 µL of the cell suspension was plated on SB plates with kanamycin and geneticin, and incubated at 37 °C for 36–48 h.

Cell toxicity studies
MTT⁹⁹ and resazurin assays⁹³,³⁰ were used to study the cell viability of M-HAp NPs using 24 well plates. Exponentially growing C. albicans cells were inoculated (5 × 10⁵ cells per well) in SB. The culture was treated with various concentrations (10, 50, 100, 500 and 1000 µg mL⁻¹) of M-HAp NPs dispersed in PBS, incubated for 12, 24 and 36 h, followed by addition of 1 mL of SB/M.M media and incubated at 37 °C on a shaking incubator for 1 h. The medium was aspirated out carefully without disturbing the cells after 4 h. The formazan crystals formed were dissolved by adding 150 µL of DMSO, and the absorbance was measured at 570 nm using a UV-visible spectrophotometer (UV-2450, Shimadzu, Japan). All the measurements were carried out in triplicate. The relative cell viability (%) was calculated as \( \frac{[A_t]/[A_c]}{100} \), where \([A_t]\) is the absorbance of the test sample and \([A_c]\) is the absorbance of the cells without treatment.

For the resazurin assay, a similar protocol was followed, wherein the resazurin dye (10 µL of 5 mg mL⁻¹) was added to the test samples after the respective incubation periods mentioned above followed by incubation at 37 °C for 4 h. The absorbance was measured at 560 nm and the relative cell viability (%) was calculated as mentioned above.

Statistical analysis
All the experiments were carried out in triplicate on different days. The results are expressed as mean ± standard error. Statistical analysis was carried out using Microsoft™ Excel 2007 software. A one-way analysis of variance (ANOVA) test was used for comparison of differences between the multiple tests. Two tailed Student’s t-test was used to analyze any significant differences between the control and individual experimental groups. ‘p’ values of less than 0.05 \((p < 0.05)\) were considered significant.

Results and discussion

Synthesis and characterization
A modified sol gel method was used to synthesize arginine (R), glucose (G) and PEG functionalized HAp NPs (M-HAp NPs) at room temperature.⁷⁷ Surface functionalization of HAp was carried out with the hypothesis that arginine, a positively charged amino acid could provide a cationic surface to facilitate efficient binding of pDNA, glucose, an essential carbon source for growth, could enhance the uptake of the NP–pDNA complex, and PEG could help pDNA to increase the interaction with the surface of the yeast cells and enhance the transformation efficiency.¹³,¹⁴,¹⁶,¹¹

The crystalline nature of HAp was confirmed by XRD analysis. The XRD spectra of HAp and M-HAp NPs were similar showing characteristic peaks at 25.8°, 31.34°, 31.95° and 33.97° corresponding to \([hkl]\) values of [002], [211], [112] and [300], respectively (Fig. 1a), confirming the formation of a hexagonal crystalline phase (ICDD 09-0432). FTIR studies were carried out to identify various functional groups associated with HAp wherein signature peaks were noted (Fig. 1b). The bands at ~600 cm⁻¹ are attributed to the bending modes of P-O bonds in phosphate groups, with contribution from –OH of the apatite group at ~605 cm⁻¹. The bands in the region of 3400 cm⁻¹ are attributed to –OH bonds and those observed near ~3571 cm⁻¹ are associated with the –OH stretching vibration of HAp.²⁷,³⁶–³⁸ In M-HAp, additional bands corresponding to glucose, arginine and PEG were also observed. The bands of NH₂ and amide I associated with arginine were observed at ~1448 and ~1644 cm⁻¹, respectively.²⁶,³²,³³,³⁹,⁴⁰ The bands corresponding to –CH of glucose and C=O–C stretching bands of PEG were observed at ~2943 cm⁻¹ and ~1100 cm⁻¹ respectively (Fig. 1c).²⁸,⁴⁰

The morphology of HAp NPs and M-HAp NPs was studied using TEM. Modification with PEG increased the average particle length from 62.5 to 72.7 nm and the diameter from 6.2 to 8.3 nm (Fig. 3). The increase in particle size as a result of PEGylation is dependent on the molecular weight of the PEG molecule. PEGylation with high molecular weight PEG contributes towards a larger increase in size as compared to low molecular weight PEG, and this is attributed to the length of the PEG chain.⁴¹–⁴⁵ In this study, PEGylation was carried out using PEG of low molecular weight (6000 kDa) resulting in a minimal increase in size (Fig. 1c).

XPS studies were carried out to determine characteristic elements of HAp and M-HAp NPs. Spectra of HAp and M-HAp NPs were similar and peaks of calcium, phosphate, and oxygen were obtained for both the samples. The presence of arginine, glucose and PEG in M-HAp NPs could not be confirmed by XPS probably due to the low dopant concentration (0.1 wt% arginine, 0.3 wt% glucose (G) and 0.05 wt% PEG).
Zeta potential measurements of HAp and M-HAp NPs were carried out to measure the surface charge. The zeta value for HAp was $\sim +13.25$ mV which increased to $\sim +72$ mV for M-HAp NPs. The increase in the zeta value noted after the functionalization of HAp could be attributed to the binding of the $\alpha$-carboxylate group of arginine and OH$^-$ ions of PEG to calcium ions of HAp such that the positively charged amino groups of arginine and H$^+$ ions of PEG are exposed at the NP/solvent interface thereby increasing the zeta potential values.$^{26,40}$ A decrease in the negative surface charge after functionalization with arginine/PEG has been observed in many NPs such as gold, silica, Fe$_3$O$_4$, etc.$^{42-45}$

**Binding efficiency of M-HAp NPs**

Binding of pDNA to NPs is essential for their proposed application of yeast transformation. The loading capacity of pDNA onto the NPs is dependent on the NP concentration and is critical in controlling the transformation efficiency. Therefore, we examined the binding efficiency (B.E) of pDNA to M-HAp NPs by measuring the absorbance of unbound pDNA at 260 nm at various NP : pDNA ratios. The B.E of pDNA to M-HAp NPs was $\sim 70\%$ when the ratio was 10 : 1 and 30 : 1, and increased to $\sim 90\%$ when the ratio was 50 : 1, 70 : 1 and 100 : 1 (Fig. 2a).

![Fig. 1](image1.png)

**Fig. 1** (a) XRD pattern, (b) FTIR spectra and (c) TEM micrographs of (i) HAp NPs and (ii) M-HAp NPs. Characteristic XRD peaks of HAp NPs were observed in all the samples. FTIR spectra showed characteristic bands of HAp, amide I, amide II, NH$_2$ glucose and PEG. TEM morphology shows M-HAp NPs with an average length and diameter of 72.7 nm and 8.3 nm.

![Fig. 2](image2.png)

**Fig. 2** (a) The percentage of bound pDNA quantified using UV absorbance at increasing NP : pDNA ratios. (b) Agarose (0.8%) gel electrophoresis of the M-HApNP–DNA complex with varied NP : pDNA ratios, lane (i) 10 : 1, lane (ii) 50 : 1, lane (iii) 70 : 1, lane (iv) 100 : 1 and lane (v) control pDNA.
pDNA to M-HAp NPs was confirmed by agarose gel electrophoresis of the complexes. In Fig. 2b, lanes [i–iv] show pDNA-M-HAp NP complexes with ratios of 10 : 1, 50 : 1, 70 : 1, and 100 : 1, demonstrating the binding of pDNA with M-HAp NPs; lane (v) is the control naked pDNA. Calcium phosphate/HAp NPs are being explored for transfection as they exhibit binding affinity for DNA, forming complexes.24,25 Increased B.E of DNA with various NPs such as HAp, chitosan and gold has been reported after functionalization with amino acids/PEG/polyethylenimine molecules.26,27

**Dynamic light scattering**

Dynamic light scattering was carried out to study the hydrodynamic radius and aggregation of M-HAp NPs and M-HAp NP–pDNA complexes in various media such as PBS, M.M and S.B (Table 1). M-HAp NPs and M-HAp NP–pDNA complexes dispersed in S.B media showed almost 3 times larger size than those in M.M and PBS medium. SB being a complex medium has a higher concentration of bio-micromolecules like peptides, lipids and electrolytes which adsorb onto the NP surface facilitating aggregation due to interparticle interaction.28,29

**Yeast transformation**

M-HAp NPs were used to transform pDNA using *C. albicans* as the model organism. The transformation process was carried out at various M-HAp NP : pDNA ratios (0 : 1, 10 : 1, 30 : 1, 50 : 1, 70 : 1 and 100 : 1), using S.B and M.M media, to obtain the optimum ratio for the maximum T.E (Table 2). Two different media were used to observe the influence/effect of media components on the transformation efficiency. In M.M media, the T.E at a NP : pDNA ratio of 10 : 1 was 10^3 cfu µg^-1, and increased to 10^6 cfu µg^-1 for a ratio of 70 : 1, beyond which it remained constant. Similarly, in S.B media the initial T.E obtained at a ratio of 10 : 1 was 37 cfu µg^-1, and increased to 10^4 cfu µg^-1 for 70 : 1 and remained constant thereafter. In M.M media, the T.E was higher by two orders of magnitude as compared to that in the complex S.B media. This could be attributed to the aggregation of NPs in complex media as observed in DLS studies (Table 1). Moreover, the presence of low concentrations of nutrients in M.M may contribute towards increased uptake of glucose functionalized HAp NP–pDNA complexes resulting in an enhanced T.E. Since the maximum T.E was obtained for a M-HAp NP : pDNA ratio of 70 : 1, it was considered optimal and used for comparison with the commonly used transformation technique of electroporation.

Table 1 Dynamic light scattering studies of R-G-HAp NPs and R-G-HAp NP–pDNA complexes in various media such as PBS, M.M and S.B

| Media   | M-HAp NPs [nm] | M-HAp NP–pDNA complex [nm] |
|---------|----------------|------------------------------|
| PBS     | 97             | 107                          |
| M.M     | 100            | 112                          |
| S.B     | 329            | 337                          |

Table 2 Transformation efficiencies of *C. albicans* obtained using modified–HApNs of various NP : pDNA ratios

| M-HAp NP : pDNA | T.E of *C. albicans* (cfu µg^-1) |
|-----------------|---------------------------------|
|                 | M.M | SB |
| 0 : 1           | 0   | 0  |
| 10 : 1          | 10^3 | 37 |
| 30 : 1          | 6 x 10^4 | 7 x 10^3 |
| 50 : 1          | 2 x 10^5 | 10^4 |
| 70 : 1          | 3 x 10^6 | 10^4 |
| 100 : 1         | 5 x 10^6 | 3 x 10^4 |

Table 3 Transformation efficiencies of *C. albicans* obtained using the nanoparticle mediated (HAp and M-HAp) and electroporation method

| Method          | T.E of *C. albicans* (cfu µg^-1) |
|-----------------|---------------------------------|
|                 | M.M | SB |
| HAp NPs        | 6 x 10^3 | 70 |
| M-HAp NPs      | 3 x 10^6 | 104 |
| Electroporation| 5 x 10^6 | 103 |

As hypothesized, the functionalization of HAp with arginine, glucose and PEG molecules enhanced the T.E. In our previous study, the strategy of glucosylation was successfully used to enhance the uptake and T.E of pDNA in bacterial cells.30 The role of glucosylation in drug delivery for improved uptake in the treatment of cancer has been explored earlier.31,32 PEGylation and functionalization of NPs with various amino acids (arginine, lysine, valine, etc.) to increase cellular uptake have also been explored for a variety of applications such as drug delivery, gene delivery and bioimaging.33,34 The potential of PEG to increase the transformation efficiency in yeast/bacteria has been demonstrated. PEG has also been used in the LiAc method to achieve a high transformation efficiency in *Saccharomyces cerevisiae*.13–15 Fluorescence microscopy studies of pDNA transformation using the LiAc method have shown that pDNA was able to bind to the yeast cell surface only in the presence of PEG, and no transformants were obtained in the absence of PEG.35 In the present study, the positively charged pDNA–M-HAp NP complex possibly attaches to the negatively charged cell surface of *C. albicans* by electrostatic attraction, facilitating cellular uptake. The possible entry of these complexes through nanopores present on the cell surfaces of the yeast cells could also be a contributing factor.
Plasmid isolation from transformed *C. albicans*

Fig. 4 shows the agarose gel image of pDNA isolated from transformed *C. albicans* using M-HAp NPs (lane i) and using the control method of electroporation by growing the cells on SB plates containing kanamycin and geneticin which was similar to that of the control pDNA (lane ii). This confirmed M-HAp NP mediated yeast transformation.

**Cell toxicity**

Biocompatibility is an important prerequisite for the successful use of NPs for transformation. To determine the effect of M-HAp NPs on the viability of *C. albicans*, time and dose dependent studies were carried out using MTT and resazurin assays (Fig. 5a and b). Cell growth was reduced by ~3-5% at concentrations above 500 \( \mu \text{g mL}^{-1} \). No significant difference (\( p > 0.05 \)) in cell viability was noted between M-HAp NPs and the untreated control at various concentrations (10, 50, 100, 500 and 1000 \( \mu \text{g mL}^{-1} \)), indicating the biocompatibility of M-HAp NPs.

HAp is a well-studied biocompatible material and its non-toxic nature has been examined on various cell lines.\(^{27,32,39,40}\) It has also been reported that functionalization of NPs with PEG makes them biocompatible by preventing agglomeration and surface oxidation.\(^{34,44}\)
Conclusion

This study demonstrated that appropriately functionalized HAp NPs can serve as a vehicle for plasmid transformation in C. albicans. Functionalization of HAp NPs with the positively charged amino acid, arginine, and PEG increased the zeta potential as well as the binding efficiency of the nanovehicle to pDNA. Modification of HAp NPs resulted in a high binding efficiency (93%) and successful transformation in C. albicans with a T.E of 10^6 cfu µg^-1. This nanovehicle delivery system does not require preparation of competent cells and is also non-toxic to yeast cells. This new method could provide exciting opportunities for the advancement of the applications of yeast in the field of biotechnology.

Ethical statement

This article does not contain any studies with human participants and animals performed by any of the authors.

Conflicts of interest

The authors declare that they have no conflict of interest.

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References

1 J.-L. Legras, D. Merdinoglu, J. Cornuet and F. Karst, Mol. Ecol., 2007, 16, 2091–2102.
2 D. Sicard and J.-L. Legras, C. R. Biol., 2011, 334, 229–236.
3 D. Botstein and G. R. Fink, Genetics, 2011, 189, 695–704.
4 V. Khurana and S. Lindquist, Nat. Rev. Neurosci., 2010, 11, 436–449.
5 S. Tenreiro, M. C. Munder, S. Alberti and T. F. Outeiro, J. Neurochem., 2013, 127, 438–452.
6 A. L. Demain and P. Vaishnav, Biotechnol. Adv., 2009, 27(3), 297–306.
7 V. Meyer, Biotechnol. Adv., 2008, 26, 177–185.
8 K. Ino, Y. Kitagawa, T. Watanabe, H. Shiku, M. Koide, T. Itayama, T. Yasukawa and T. Matsue, Electrophoresis, 2009, 30, 3406–3412.
9 D. Pompon, A. Perret, A. Bellamine, R. Laine, J. C. Gautier and P. Urban, Toxicol. Lett., 1995, 82, 815–822.
10 M. S. Siddiqui, K. Thodey, I. Trenchard and C. D. Smolke, FEMS Yeast Res., 2012, 12(2), 144–170.
11 D. M. Becker and L. Guarente, Methods Enzymol., 1991, 194, 182–187.
12 R. A. Butow, R. M. Henke, J. V. Moran, S. M. Belcher and P. S. Perlman, Methods Enzymol., 1996, 264, 265–278.
13 R. D. Gietz and R. H. Schiestl, Nat. Protoc., 2007, 2, 31–34.
14 R. D. Gietz and R. H. Schiestl, Nat. Protoc., 2007, 2, 38–41.
15 R. D. Gietz and R. A. Woods, Yeast Protoc., 2006, vol. 313, pp. 107–120.
16 R. J. Klebe, J. V. Harriss, Z. D. Sharp and M. G. Douglas, Gene, 1983, 25, 333–341.
17 N. Yoshida, T. Ikeda, T. Yoshida, T. Sengoku and K. Ogawa, FEMS Microbiol. Lett., 2001, 195, 133–137.
18 A. Bozkir and O. M. Saka, J. Drug Targeting, 2004, 12, 281–288.
19 H. Tan, L. Fu and M. Seno, Int. J. Mol. Sci., 2010, 11, 4962–4972.
20 D. R. Radu, C. Y. Lai, K. Jeftinija, E. W. Rowe, S. Jeftinija and V. S. Y. Lin, J. Am. Chem. Soc., 2004, 126, 13216–13217.
21 I. L. Slowing, J. L. Vivero-Escoto, C. W. Wu and V. S. Y. Lin, Adv. Drug Delivery Rev., 2008, 60, 1278–1288.
22 Y. Filyak, N. Finiuk, N. Mitina, O. Bilyk, V. Titorenko, O. Hrydzhuk, A. Zaichenko and R. Stoika, BioTechniques, 2013, 54, 35–43, DOI: 10.2144/000113980.
23 S. Naqvi, A. Maitra, M. Abdin, M. Akmal, I. Arora and M. Samim, J. Mater. Chem., 2012, 22, 3500–3507.
24 T. N. Tram Do, W.-H. Lee, C.-Y. Loo, A. V. Zavgorodniy and R. Rohanizadeh, Ther. Delivery, 2012, 3(5), 623–632.
25 V. Uskoković and D. P. Uskoković, J. Biomed. Mater. Res., Part B, 2011, 96, 152–191.
26 Z. Yan-Zhong, H. Yan-Yan, Z. Jun, Z. Shai-Hong, L. Zhi-You and Z. Ke-Chao, Nanoscale Res. Lett., 2011, 6, 1–8.
27 K. Deshmukh, M. M. Shaik, S. R. Ramanan and M. Kowshik, ACS Biomater. Sci. Eng., 2016, 2(8), 1257–1264.
28 D. Olton, J. Li, M. E. Wilson, T. Rogers, J. Close, L. Huang, P. N. Kumta and C. Sfeir, Biomaterials, 2007, 28, 1267–1279.
29 D. Gerlier and N. Thomassett, J. Immunol. Methods, 1986, 94, 57–63.
30 S. D. Sarker, L. Nahar and Y. Kumarasamy, Methods, 2007, 42, 321–324.
31 S. Zhu, B. Huang, K. Zhou, S. Huang, F. Liu, Y. Li, Z. Xue and Z. Long, J. Nanopart. Res., 2004, 6, 307–311.
32 R. Gonzalez-McQuire, J.-Y. Chane-Ching, E. Vignaud, A. Lebugle and S. Mann, J. Mater. Chem., 2004, 14, 2277–2281.
33 T. Matsumoto, M. Okazaki, M. Inoue, Y. Hamada, M. Taira and J. Takahashi, Biomaterials, 2002, 23, 2241–2247.
34 G. D. Venkatasubbub, S. Ramasamy, G. Avadhani, V. Ramakrishnan and J. Kumar, Powder Technol., 2013, 235, 437–442.
35 X. Zhang, J. Hui, B. Yang, Y. Yang, D. Fan, M. Liu, L. Tao and Y. Wei, Polym. Chem., 2013, 4, 4120–4125.
36 S. Jadallagnagari, K. Deshmukh, S. R. Ramanan and M. Kowshik, Appl. Nanosci., 2014, 4, 133–141.
37 S. Jadallagnagari, K. Deshmukh, A. K. Verma, R. Vohra, M. Kowshik and S. Roy Ramanan, Sci. Adv. Mater., 2014, 6, 312–319.
38 S. R. Ramanan and R. Venkatesh, Mater. Lett., 2004, 58, 3320–3323.
39 S. Ueno and S. Shimabayashi, Phosphorus Res. Bull., 2009, 23, 57–62.
40 G. H. Wang, Y. Z. Zhao, T. Juan, S. H. Zhu and K. C. Zhou, Trans. Nonferrous Met. Soc. China, 2015, 25, 490–496.
41. M. Ibrahim, M. Alaam, H. El-Haes, A. F. Jalbout and Ad. Leon, *Ecletica Quim.*, 2006, **31**, 15–21.
42. M. Anbarasu, M. Anandan, E. Chinnasamy, V. Gopinath and K. Balamurugan, *Spectrochim. Acta, Part A*, 2015, **135**, 536–539.
43. T. Andreani, A. L. R. De Souza, C. P. Kiill, E. N. Lorenzón, J. F. Fanguieiro, A. C. Calpena, M. V. Chaud, M. L. Garcia, M. P. D. Gremião and A. M. Silva, *Int. J. Pharm.*, 2014, **473**, 627–635.
44. J. Manson, D. Kumar, B. J. Meenan and D. Dixon, *Gold Bull.*, 2011, **44**, 99–105.
45. B. Pelaz, P. Del Pino, P. Maffre, R. Hartmann, M. Gallego, S. Rivera-Fernandez, J. M. de la Fuente, G. U. Nienhaus and W. J. Parak, *ACS Nano*, 2015, **9**, 6996–7008.
46. B. Layek and J. Singh, *Biomacromolecules*, 2013, **14**(2), 485–494.
47. P. S. Ghosh, C. K. Kim, G. Han, N. S. Forbes and V. M. Rotello, *ACS Nano*, 2008, **2**(11), 2213–2218.
48. L. Wu, J. Xie, T. Li, Z. Mai, L. Wang, X. Wang and T. Chen, *R. Soc. Open Sci.*, 2017, **4**(10), 170822.
49. K. Rausch, A. Reuter, K. Fischer and M. Schmidt, *Biomacromolecules*, 2010, **11**(11), 2836–2839.
50. T. L. Moore, L. Rodriguez-Lorenzo, V. Hirsch, S. Balog, D. Urban, C. Jud, B. Rothen-Rutishauser, M. Lattuada and A. Petri-Fink, *Chem. Soc. Rev.*, 2015, **44**, 6287–6305.
51. K. Deshmukh, S. R. Ramanan and M. Kowshik, *Mater. Sci. Eng., C*, 2019, **96**, 58–65.
52. X. Jiang, H. Xin, Q. Ren, J. Gu, L. Zhu, F. Du, C. Feng, Y. Xie, X. Sha and X. Fang, *Biomaterials*, 2014, **35**, 518–529.
53. J. Wang, C. Yin, G. Tang, X. Lin and Q. Wu, *Int. J. Pharm.*, 2013, **441**, 291–298.
54. J. V. Jokerst, T. Lobovkina, R. N. Zare and S. S. Gambhir, *Nanomedicine*, 2011, **6**, 715–728.
55. P. Chen, H.-H. Liu, R. Cui, Z.-L. Zhang, D. W. Pang, Z. X. Xie, H. Z. Zheng, Z. X. Lu and H. Tong, *Talanta*, 2008, **77**, 262–268.