Rapid adaptation of multisensory integration in vestibular pathways

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Sensing gravity is vital for our perception of spatial orientation, the control of upright posture, and generation of our everyday activities. When an astronaut transitions to microgravity or returns to earth, the vestibular input arising from self-motion will not match the brain's expectation. Our recent neurophysiological studies have provided insight into how the nervous system rapidly reorganizes when vestibular input becomes unreliable by both (1) updating its internal model of the sensory consequences of motion and (2) up-weighting more reliable extra-vestibular information. These neural strategies, in turn, are linked to improvements in sensorimotor performance (e.g., gaze and postural stability, locomotion, orienting) and perception characterized by similar time courses. We suggest that furthering our understanding of the neural mechanisms that underlie sensorimotor adaptation will have important implications for optimizing training programs for astronauts before and after space exploration missions and for the design of goal-oriented rehabilitation for patients.

Keywords: vestibule, vestibular nuclei, astronauts, internal model, vestibular diseases, sensorimotor, adaptation, sensory reweighting

Introduction

On earth, gravity provides a unique reference axis to which we can anchor our body orientation and monitor orientation changes. Indeed, as Lacquaniti et al. (2004) have noted, it is a force to which we are constantly exposed starting from the day we are born. The findings of theoretical as well as behavioral studies have led to the longstanding hypothesis that the brain builds an internal model of the expected sensory consequence of our own actions (Wolpert et al., 1998; Wolpert and Ghahramani, 2000; Herzfeld et al., 2014)—which is required for accurate spatial orientation, the control of posture, and the generation of precise movements. On earth, the expectation of the constant force of gravity is an inherent component of this internal model. By combining the information available from different modalities (i.e., the vestibular, proprioceptive and somatosensory as well as the visual systems) with its internal model, the brain can sense and anticipate the consequences of the force of gravity (reviewed in McIntyre et al., 1998; Zupan et al., 2002). During space exploration missions, however, gravity becomes minimal resulting in a mismatch between the brain's expectation of sensory consequence of movement and that actually experienced. This has important implications for astronauts. Specifically, astronauts show impaired balance, locomotion, gaze control, dynamic visual acuity, eye–head–hand coordination during the space flight (reviewed in Souvestre et al., 2008).

The effects of this decrease in gravity are most pronounced immediately after the transition to microgravity (Montgomery et al., 1993). When moving, astronauts not only experience impairments in sensorimotor performance but also report spatial disorientation and destabilizing sensations such as the feeling of having suddenly turned upside-down and/or difficulty in sensing the
location of their own arms and legs (Souvestre et al., 2008). It is generally thought that these symptoms arise because the integration of sensory input from the vestibular system with that from the proprioceptive, somatosensory, and visual systems misinforms the brain relative to its existing (i.e., earth-based) “internal” model of the expected sensory consequences of motion (Freeman, 2000). This conflict between the brain’s expectation of sensory feedback and the actual sensory feedback experience in microgravity is also thought to be the cause of space motion sickness experiences during the initial stages of space flight (Freeman, 2000; Oman and Cullen, 2014). Overall, nearly 70% of all astronauts experience impaired motor performance and/or space motion sickness (Lackner and Dizio, 2006). To develop new training and treatment approaches, it is important to understand the mechanisms that underlie these symptoms as well as those that are responsible for recovery.

As discussed below, our recent work provides 2 major advances in this area. First we have shown that neurons that sense “sensory conflict” from the otoliths can be found at the first stage of central vestibular processing (i.e., vestibular nuclei; Carriot et al., 2013, 2014, 2015), and that the cerebellum plays a key role in computing the difference between expected and actual vestibular input during active motion (Brooks and Cullen, 2013). Second, our work shows that when the vestibular input experienced during motion is altered relative to normal conditions, the dynamic re-weighting of multimodal inputs enables the sensorimotor adaptation observed during behavioral recovery.

Neural Correlates of Sensorimotor Adaptation: Sensory Conflict

In single unit recording studies we have shown that a subclass of neurons in the vestibular nuclei, which project to the spinal cord and to vestibular thalamus, respond preferentially to passive head movements. For example, during everyday activities, the otoliths are activated both by gravity and by our own self-motion (Carriot et al., 2014). In response to active motion, the otolith afferents in the 8th nerve send robust signals to the vestibular nuclei (Jamali et al., 2009). However, at the next stage of processing, this “reafferent” sensory input is canceled (Carriot et al., 2013, 2015). Our recent work further suggests that this cancelation is mediated by a mechanism that compares the expected consequences of self-generated movement (computed by an internal model located in the cerebellum) and the actual sensory feedback (Figure 1A). Notably, the un-cancelled sensory input (“exafference”) resulting from passive movement is thought to allow the brain to compensate for unexpected postural disturbances and ensure perceptual stability (reviewed in Cullen, 2012). Such a mechanism is similarly consistent with the observation that impairments in balance, locomotion, gaze control, dynamic visual acuity, eye–head–hand coordination and perception are most serious during the initial phase of space flight and re-entry. Once the brain’s internal model had been updated to account for the change in the forces gravity, it learns to expect a different pattern of input from the 8th nerve during motion that again ensures accurate motor control and perceptual stability.

Neural Correlates of Sensorimotor Adaptation: Dynamic Re-Weighting of Multimodal Inputs

Indeed, although the symptoms of space motion sickness/spatial disorientation can initially be quite debilitating, they decrease over time (from 1 h to 4 days) such that astronauts are able to comfortably make voluntary head movements during a mission. Astronauts again experience these symptoms upon returning to Earth’s 1-g environment. Because access to astronauts is more straightforward in this latter condition, it is more often the focus of quantitative studies. Interestingly, aspects of the motor performance observed after returning to 1-g environment astronauts are similar to those observed in the patients from acute unilateral vestibular peripheral loss (see also Mulavara et al., 2012). In both conditions, the actual vestibular feedback experienced during self-motion is initially different from that which is expected. Recent studies in our laboratory have provided insights into the neural mechanisms that underlie the adaptation of the sensorimotor integration following peripheral vestibular loss (Sadeghi et al., 2010, 2011, 2012; Jamali et al., 2014).

In particular, we discovered that compensation is mediated by the dynamic reweighting of inputs from different modalities (i.e., extravestibular versus vestibular) at the level of the single neurons that constitute the first central stage of vestibular processing. At least two types of extravestibular inputs can substitute for the lost vestibular input, (1) proprioception and (2) motor efference copy signals. As reviewed above, in normal conditions, vestibular responses to active motion are suppressed when there is a match between the brain’s estimate of proprioceptive feedback and the actual sensory feedback. However, under normal conditions (1) passive stimulation of neck proprioceptors in isolation does not alter neuronal responses and (2) the generation of motor efference copy signals does not alter neuronal responses when the head is prevented from moving (i.e., in this condition there is a mismatch between expected and actual feedback). In contrast, following peripheral vestibular loss, neurons respond differently. First, robust response to passive stimulation of neck proprioceptors are rapidly unmasked in the early vestibular pathway (Figure 1B, top panel, red trace), can be linked to the compensation process as evidenced by faster and more substantial recovery of the resting discharge in proprioceptive-sensitive neurons (Sadeghi et al., 2010). Furthermore, when the head is restrained neuronal responses to motor efference copy are unmasked over the course of weeks (Figure 1B, top panel, purple trace).

The Dynamics of Behavioral Adaptation: Vestibular Compensation and Re-Entry

The time course of the dynamic re-weighting of multimodal information observed at the level of single neurons, follows a similar time course to the improvement observed in (1) patient performance following vestibular loss and (2) astronaut return back to earth (Figure 1B, compare top and middle panels). First, patients generally show significant improvement in postural performance in first days after lesion, with more gradual
Carriot et al. Plasticity in the vestibular pathways

FIGURE 1 | Sensorimotor adaptation during vestibular compensation and re-entry. (A) Proposed mechanism for the selective encoding of exafference. Vestibular reafference is canceled when the actual sensory input matches the expected sensory consequence of motor command. (B) Top panel: the time course of dynamic re-weighting of multimodal inputs during vestibular compensation. Middle panel: the time course of the behavioral adaptation for vestibular patients as well as astronauts after re-entry. Bottom panel: the contribution of vestibular and neck inputs to the neuronal detection thresholds over the course of recovery after vestibular loss.

improvement seen within a 1–2 weeks (Figure 1B, middle panel, gray trace adapted from Gauchard et al., 2013). Early sensorimotor symptoms include significant head tilt in the roll plane toward the lesion and a tendency to deviate toward the lesioned side when walking (reviewed in Smith and Curthoys, 1989; Curthoys and Halmagyi, 1995). Second and similarly, astronauts show rapid sensorimotor learning in the first day after return, with more gradual improvement in the following weeks ultimately returning performance to pre-flight levels. Superimposed in Figure 1B (middle panel) for comparison is an example of the adaption that occurs following return from space flight (e.g., locomotor performance; Mulavara et al., 2010). A similar time course has been reported for balance control recovery (Paloski et al., 1992; Reschke et al., 1998), as well as perception, spatial orientation, eye–head and head–trunk coordination following re-entry (Glasauer et al., 1995; Bloomberg et al., 1997; Reschke et al., 1998; Bloomberg and Mulavara, 2003; Courtine and Pozzo, 2004; Clement and Wood, 2014).
**Neural Correlates of Perception: Dynamic Re-Weighting of Multimodal Inputs**

Recently, we have further demonstrated that, following partial vestibular loss, neurons at the first central stage of vestibular processing, in the vestibular nuclei, show increased variability in response to vestibular stimulation. This increase in variability does not improve over time and ultimately constrains neural detection thresholds (Jamali et al., 2014; Figure 1B, bottom panel, blue trace). As noted above, these neurons not only contribute to posture and balance via projections to the spinal cord, but also send information to the thalamus, and then on to regions of cerebral cortex. Accordingly, they likely make a vital contribution to the perception of spatial orientation and self-motion (reviewed in Cullen, 2012). This then raises the question: What mechanisms underlie the observed improvements in perceptual threshold? Indeed, we found that sensory substitution with extravehicular (i.e., proprioceptive; Figure 1B, bottom panel, red trace) inputs provides a neural substrate for improvements in self-motion perception following vestibular loss (e.g., Bergeurius et al., 1996; Cutfield et al., 2011; Cousins et al., 2013) which similarly shows significant improvement over this same time frame.

**Conclusions**

It is noteworthy that dynamic reweighting of extravehicular inputs occurs in the same neurons that sense “sensory conflict” during self-generated motion—namely at the first stage of central vestibular processing. Thus, sensorimotor adaptation in conditions where sensory input is altered (e.g., after vestibular loss of function or experiencing a new gravitational environment) appears to involve the simultaneous updating of internal models and the dynamic re-weighting of multimodal input. We speculate that the central nervous system utilizes a similar multimodal strategy to compensate for changes in gravity, experienced in both of these conditions. Our recent neurophysiological findings further provide a neural correlate for the benefits provided by rehabilitative strategies that take advantage of the convergence of multisensory cues during sensorimotor adaptation following vestibular loss. For example, standard rehabilitation techniques aimed at improving balance such as Caithorne–Cooksey exercises incorporate the generation of head and body movements, which essentially provides multimodal stimulation (i.e., combined vestibular and proprioceptive; reviewed in Ricci et al., 2010).

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