CT Perfusion in Acute Lacunar Stroke: Detection Capabilities Based on Infarct Location

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ORIGINAL RESEARCH

CT Perfusion in Acute Lacunar Stroke: Detection Capabilities Based on Infarct Location

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ABSTRACT

BACKGROUND AND PURPOSE: Recent studies demonstrated superiority of CTP to NCCT/CTA at detecting lacunar infarcts. This study aimed to assess CTP’s capability to identify lacunae in different intracranial regions.

MATERIALS AND METHODS: Over 5.5 years, 1085 CTP examinations were retrospectively reviewed in patients with acute stroke symptoms with CTP within 12 hours and MRI within 7 days of symptom onset. Patients had infarcts ≤2 cm or no acute infarct on DWI; patients with concomitant infarcts >2 cm on DWI were excluded. CTP postprocessing was automated by a delay-corrected algorithm. Three blinded reviewers were given patient NIHSS scores and symptoms; infarcts were recorded based on NCCT/CTA, CTP (CBF, CBV, MTT, and TTP), and DWI.

RESULTS: One hundred thirteen patients met inclusion criteria (53.1% female). On DWI, lacunar infarcts were present in 37 of 113 (32.7%), and absent in 76 of 113 (67.3%). On CTP, lacunar infarcts typically appeared as abnormalities larger than infarct size on DWI. Interobserver $\kappa$ for CTP ranged from 0.38 (CBF) ($P < 0.0001$) to 0.66 (TTP) ($P < 0.0001$); interobserver $\kappa$ for DWI was 0.88 ($P < 0.0001$). In all intracranial regions, sensitivity of CTP ranged from 18.9% (CBV) to 48.7% (TTP); specificity ranged from 97.4% (CBF and TTP) to 98.7% (CBV and MTT). CTP’s sensitivity was highest in the subcortical white matter with or without cortical involvement (21.7%–65.2%) followed by periventricular white matter (12.5%–37.5%); sensitivity in the thalami or basal ganglia was 0%.

CONCLUSIONS: CTP has low sensitivity and high specificity in identifying lacunar infarcts. Sensitivity is highest in the subcortical white matter with or without cortical involvement, but limited in the basal ganglia and thalamai.

ABBREVIATIONS: CTP = computed tomography perfusion; NCCT = noncontrast computed tomography; DWI = diffusion-weighted imaging; CTA = computed tomography angiography; CBF = cerebral blood flow; CBV = cerebral blood volume; MTT = mean transit time; TTP = time to peak; CSWM = subcortical white matter with or without involvement of the cortex; PVWM = periventricular white matter.
ther study investigated CTP’s capability to detect lacunae within specific regions of the brain.

The purpose of this study was to compare the diagnostic performance of CTP with NCCT/CTA in the identification of acute lacunar infarcts and evaluate the diagnostic capabilities of CTP in the detection of lacunar strokes within different areas of the brain.

**MATERIALS AND METHODS**

**Patient Selection**

This study was completed at a level 1 trauma center and primary stroke center. Institutional review board approval was obtained for this study. A retrospective review of all patients who presented with symptoms of acute stroke between January 2006 and July 2011 was performed; 1085 patients with CTP examinations were identified. Patients were included if they underwent acute CTP imaging within 12 hours of symptom onset, as well as DWI within 7 days of presentation. One investigator manually measured the longest axial diameter of foci of restricted diffusion on DWI, if present. Patients were included if they had either 1) negative DWI or 2) one or more infarcts <20 mm in maximum diameter on DWI. The size of 20 mm as the uppermost criterion for lacunar infarcts was chosen based on prior studies implicating this as a clinically applicable measurement.4,16 Exclusion criteria were: 1) infarct >20 mm in diameter, 2) lacunar stroke with coexisting large (>20 mm maximum diameter) infarct, 3) nonoptimal quality of either CTP or DWI (eg, technical problems such as motion), and 4) administration of intravenous tPA between the time of CTP and DWI acquisitions.

**DWI and CTP Acquisition and Postprocessing**

MR imaging scans were performed on 2 different scanners (Ingenia 1.5T and Ingenia 3T MR scanners; Philips Medical Systems, Best, the Netherlands). On the 1.5T scanner, the sequence parameters were: TR = 3526, TE = 92, flip angle = 90°, EPI factor = 45, 2.4 acceleration (SENSE) factor, 3 directions of measurement, 16 cm FOV, 131 × 131 matrix, 5-mm section thickness. On the 3T scanner, the sequence parameters were: TR = 3832, TE = 84, flip angle = 90°, EPI factor = 51, 2.4 acceleration (SENSE) factor, 3 directions of measurement, 14 cm FOV, 152 × 121 matrix, 4-mm section thickness. Both scanners used 16-channel head coils. Foci of diffusion were measured in the longest axial axis. DWI b-value was b = 1000 for all studies.

Every patient was imaged as part of the same protocol used for emergent strokes at our institution: an NCCT was immediately followed by multidetector CTA; CTP images were obtained <5 minutes later. For NCCT, FOV was 25 cm, with 512 × 512 matrix and 3-mm sections; for CTA, FOV was 22 cm, with 512 × 512 matrix and 0.9-mm sections. CTA is performed before CTP to minimize venous contamination on CTA scans; in several years’ experience with this imaging protocol, the venous contamination noted on CTP images is minimal.15 CTP images were not obtained if hemorrhage was visualized on the NCCT by the daytime hours staff, on-site radiology resident, or neuroradiology fellow; patients with hemorrhage did not meet the study’s inclusion criteria.

A 64-section multidetector scanner was used to perform all CT scans (Brilliance CT; Philips Medical Systems). All CTP sequences were completed by using 2 first-pass acquisitions of sequential 55–60 second dynamic injections/scans (1 image/s) with no delay between the acquisitions. Two acquisitions were completed because each included 40 mm of coverage; hence, 1 acquisition was set at the level of the basal ganglia, and the second was set at the level of the superior margin of the ventricles. According to the manufacturer, 55–60 second dynamic acquisitions were used based on several years’ experience before this study of dynamic timing that minimized truncation effect. A truncation is applied to recirculation for the computation of CBV, with only the first-pass contrast taken into account for CBV. Each acquisition yielded 4 contiguous sections (25 cm FOV, 512 × 512 matrix, 10-mm section thickness, 32 × 1.25 mm collimation, 80 kV, 120 mAs), with a total of 40 mm of coverage. A bolus of 36–40 mL of nonionic contrast (iohexol [Omnipaque 350 mg/mL; GE Healthcare, Piscataway, New Jersey]) was intravenously administered for each acquisition via a power injector at a rate of 6.0 mL/s for a total of 72–80 mL of intravenous contrast for each CTP scan. A saline flush was administered between the acquisition of CTA and CTP imaging, but not between the 2 CTP acquisitions. Typically, the inferior margins of each CTP acquisition were the inferior margin of the basal ganglia and the midventricle semiovale superiorly. The margins were occasionally adjusted if a suspected infarct was identified on the NCCT by the radiology resident or neuroradiology fellow.

CTP postprocessing was completed on a Vitrea workstation (Vital Images, Minnetonka, Minnesota). CTP postprocessing was automated by a delay-corrected singular value decomposition algorithm; the workstation’s postprocessing software uses a deconvolution-based delay-corrected singular value decomposition algorithm via interhemispheric comparison (side-to-side). The interhemispheric comparison performed by the postprocessing software is done by using a multistep approach: 1) the midline of the brain is automatically located (but can be manually corrected, if necessary), 2) the affected side is automatically identified by using TTP maps, and 3) MTT, TTP, CBV, and CBF in the affected side are automatically compared with the corresponding parameters in the contralateral side by using relative differences between each voxel. Arterial input functions were selected from the anterior cerebral artery, and venous functions were selected from the posterior segment of the superior sagittal sinus; automatic selection was used, which was verified before the finalization of images.

**Image Review and Interpretation**

Three staff neuroradiologists (2 with >10 years’ experience, 1 with 1.5 years’ experience), who had been blinded to the final results, independently reviewed the DWI, NCCT, CTA, and CTP images. Each reviewer was given the patient NIHSS score and symptoms at the time of presentation; the reviewers were otherwise blinded to the patient interpretative reports and the other reviewers’ interpretations. The neuroradiologists assessed for the presence of stroke by using 4 different independent CTP parameters: CBF, CBV, MTT, and TTP. Presence or absence of stroke was then assessed on all imaging sequences; NCCT, CTA, and CTP images were reviewed first, and DWI was reviewed afterward to blind the review of CTA and perfusion data to the DWI results. Stroke locations were divided into the subcortical white matter...
with or without involvement of the overlying cortex (CSWM), periventricular white matter (PVWM), basal ganglia and/or thalamus, cerebellum, and brain stem. Brain stem and cerebellar infarcts \( (n = 9) \) were ultimately excluded because the CTP margins did not extend inferiorly enough to encompass strokes in those locations; 1 infarct in the PVWM was also excluded because the CTP images did not fully include the infarct. Interpretations were considered correct if 2 or more reviewers agreed on the results.

NCCT/CTA and CTP findings were subsequently compared with DWI. Using DWI as the “criterion standard,” findings were denoted as true-positive results if: 1) the abnormalities on NCCT/CTA corresponded with the same areas as the infarcts on DWI or 2) regional abnormalities on CTP included the area of lacunar infarction on DWI. Abnormalities on NCCT/CTA and CTP were marked as false-positives if: 1) no infarct was present on DWI or 2) the infarct on DWI was in a different location than that of the CTP. A single neuroradiologist graded the amount of chronic small vessel ischemic disease based on a grading scale: 1 (none-minimal), 2 (mild-moderate), 3 (moderate), 4 (moderate-severe), and 5 (severe).

### Statistical Analysis

Intra- and interobserver agreement was calculated by using the Cohen \( \kappa \). The sensitivity and specificity of the NCCT/CTA and independent CTP parameters (CBF, CBV, MTT, and TTP) in each area of the brain (basal ganglia and/or thalamus, CSWM, PVWM) were calculated. A \( P \) value of <.05 was considered statistically significant. Statistical analysis was performed by using Statistical Analysis Software (SAS; SAS Institute, Cary, North Carolina). Charts were created in Microsoft PowerPoint Version 14.6 (Microsoft, Redmond, Washington).

### RESULTS

#### Patient Population

One hundred sixty patients underwent CTP imaging within 12 hours and DWI within 7 days of symptom onset, with or without lacunar infarction on DWI. Of these, 27 were excluded because they received tPA between the CTP and DWI, 10 were excluded because the CTP images did not adequately involve the area of infarction (9 in the brain stem or cerebellum and 1 in the PVWM), 6 were excluded because of the presence of encephalomalacia (eg, from prior stroke), 3 were excluded because the examination was limited by motion and/or other types of artifact distortion, and 1 was excluded because the abnormality was later found to be a tumor (Fig 1). Thus, 113 patients were included for this study cohort; 37 (32.7%) had infarction on DWI, and 76 (67.3%) had no infarction. The average age at onset of symptoms was 59.8 ± 16.9 years. Sixty (53.1%) of the included patients were women.

#### Infarct Timing and Locations

The average time between symptom onset to CTP imaging was 2.4 ± 1.1 hours for all patients; the average time between CTP and MR imaging was 0.9 ± 1.0 days. The average degree/grade of chronic small vessel ischemic disease on NCCT was 2.1 ± 1.3 for all patients, corresponding to approximately mild-to-moderate disease based on the grading scale used. Of the infarcts noted on DWI, 23 of 37 (62.2%) were located in the PVWM, 8 of 37 (21.6%) in the PVWM, and 6 of 37 (16.2%) in the basal ganglia and/or thalamus. The mean NIHSS score for all studied patients was 4.0 ± 5.0 (3.9 ± 5.6 for patients with infarct and 4.1 ± 4.7 for patients without infarct). Four patients received tPA before both CTP and MR imaging.

#### Imaging Results

Regarding lacunar infarcts in all locations within the brain, CTP sensitivity for the detection of lacuneae ranged from 18.9% (CBV) to 48.7% (TTP) depending on perfusion parameter. The sensitivity of NCCT/CTA was 2.7%. False-positive CTP interpretations, in which the consensus CTP was noted to be positive in a patient without infarct on DWI, were observed in all CTP sequences; no false-positive interpretation occurred in NCCT/CTA. Specificity of CTP ranged from 97.4% (CBF and TTP) to 98.7% (CBV and MTT); NCCT/CTA specificity was 100% (Table). Lacunar infarcts typically appeared on CTP images as regional abnormalities larger than the infarcts observed on DWI (Fig 2).

In all locations, the positive predictive value for CTP ranged from 81.8% (CBF) to 92.9% (MTT). The negative predictive value ranged from 71.4% (CBV) to 80.0% (TTP). Regarding interpretation of CTP images, interobserver \( \kappa \) ranged from 0.38 for CBF to 0.66 for TTP \( (P < .0001 \text{ for all}) \). Interobserver \( \kappa \) was 0.88 for DWI \( (P < .0001) \) and 0.05 for NCCT/CTA \( (P = .18) \).
Conversely, regarding the capability of CTP to detect lacunar infarcts in different intracranial regions, the sensitivity of CTP was highest in the CSWM with TTP (65.2%). Within the PVWM, CTP sensitivity was highest with TTP and MTT (37.5% for both) and lowest with CBF (12.5%) (Fig 3). None of the lacunar infarcts in the basal ganglia or thalamus were identified by using CTP (0/6). The sensitivity of NCCT/CTA for lacunar infarcts in the basal ganglia and/or thalamus was 16.7%; no lacunar infarcts were identified on NCCT/CTA in the CSWM or PVWM (0/23 and 0/8, respectively). The intracranial location with the highest sensitivity was the CSWM with MTT (90.9%).

**DISCUSSION**

This study set out to determine the capability of CTP to identify acute lacunar strokes. The results indicate that CTP has high specificity in the detection of lacunar strokes, though its sensitivity is low among all perfusion parameters. CTP is best able to detect infarcts in the CSWM, followed by the PVWM; lacunae were not accurately identified on CTP in the basal ganglia or thalamus. Overall, CTP outperformed NCCT/CTA in finding lacunar strokes. The sensitivities of TTP and MTT measured in this study were notably higher than those of CBF and CBV, consistent with past studies that have shown these parameters to be inferior to TTP and MTT as indicators of infarct.18

Over half of the lacunae noted on DWI in the present study were located in the subcortical white matter with or without involvement of the overlying cortex; the remaining infarcts were located in the PVWM, basal ganglia, and thalamus. Larger-scale studies have noted that most lacunar strokes occur in either the lentiform nuclei or thalamus.19 The small number of lentiform and or thalamic lacunae in this study might be related to a relatively small cohort. Nevertheless, it is notable that none of the infarcts in the basal ganglia or thalamus were accurately identified on CTP. The cerebellum and brainstem were not adequately covered by the CTP images and consequently were not assessed in this study, which is a limitation.

A recent study by Das et al16 indicated that CTP had added value to NCCT alone in the setting of lacunar infarcts. However, reported sensitivities of CTP for detecting strokes <2 cm have been quite variable; Mayer et al20 stated that lacunar strokes were difficult to distinguish from artifact on CTP imaging, and other authors have cited sensitivities as low as 0% and as high as 47.4%–62.5%.10,15,21 Furthermore, a systematic review by

**FIG 2.** A 49-year-old woman who presented with left-sided facial weakness and dysarthria. Infarct within the right centrum semiovale on DWI (A, white arrow) corresponded with focal abnormalities on TTP (B) and MTT (C) images (white arrow on each); the abnormalities on TTP and MTT were slightly larger than the confirmed infarct on DWI. No abnormalities were identified on CBV (D), CBF (E), or NCCT (F).

**FIG 3.** Example of a lacunar infarct not visualized on CTP images. A 74-year-old man who presented with right arm weakness. DWI confirmed a lacunar infarct in the left centrum semiovale (A, white arrow). No abnormalities were noted on NCCT (B), CTA (C), TTP (D), CBF (E), or CBV (F).
Biesbroek et al.22 noted that approximately two-thirds of false-negative findings on CTP were lacunae, and a study by Eckert et al.23 noted that the most common cause of false-negative multimodal CT imaging was lacunar infarcts. Although the reason for this inconsistency among studies is not clear, it is likely that the variability is at least in part because of differences in the designs of the studies (eg, whether there was a known lacunar stroke and whether the reviewers were blinded). In addition, the parameters used in each study, such as time-to-maximum versus TTP, might have contributed to differences in reported sensitivities. The present study provided reviewers with patient NIHSS scores as well as presenting symptoms; thus, the results of this study might better reflect the sensitivity of lacunar infarct detection in a clinical setting.

In addition, differences in reported sensitivities of lacunar infarct detection might be attributed to the use of delay-sensitive singular value decomposition algorithms in some studies. Prior studies by Sasaki et al.24 and Kudo et al.25 have demonstrated the superior accuracy of delay-corrected singular value decomposition algorithms in CTP in acute infarcts. Delay-sensitive singular value decomposition algorithms have been shown to overestimate MTT prolongation and CBF reduction in acute stroke, thus falsely increasing their sensitivity to infarcts.24 A recent study by Cao et al.26 also used delay-corrected singular value decomposition to assess for lacunar infarcts; the reviewers were similarly blinded to DWI results, but were aware of the patients’ presenting symptoms. The authors of that study reported a superior sensitivity of MTT (56%) compared with the results of the current study, but similarly noted high specificities (100% for CBV, CBF, and MTT).

Although the presence of stroke on CTP appears to be fairly specific for infarction, the infarct size on CTP often did not correlate with the focus of restricted diffusion on DWI. In many patients, the defects on CTP appeared as regional abnormalities corresponding to, but larger than, the location of the lacunar stroke. In contrast, a recent study by Rudilosso et al.15 noted focal defects on CTP that more accurately estimated infarct size on DWI. The present study did not set specific CTP thresholds, which might have contributed to the mismatch in infarct sizes observed in CTP and DWI (ie, the area of restricted diffusion might have represented the infarct “core,” whereas the observed abnormalities on CTP might have represented a wider zone of ischemia). Alternatively, abnormalities on CTP might have represented the cumulative effect of multiple lacunar infarcts within the same region; although patients with coexistent infarcts >2 cm were excluded, some patients had multiple lacunae that might have contributed to additional findings.

This study has limitations shared by any retrospective study. In addition, CTP sections did not adequately cover the brain stem or cerebellum, limiting our evaluation of its diagnostic capabilities in those regions. In addition, there was a temporal difference between the acquisition of CTP and DWI in some patients, which might have biased the results. Also, infarcts might have formed and/or increased in size between the acquisition of CTP and DWI. We sought to minimize any artifact differences by excluding patients who received iPA therapy between the 2 examinations. Next, as stated above, thresholds for CTP were not established for this study. However, the purpose of this study was to assess CTP’s ability to identify infarcts rather than measure CTP’s capability to estimate infarct core. In addition, only a small number of subjects (n = 6) had infarcts within the basal ganglia and/or thalamus, limiting the assessment of CTP capabilities within those regions. Finally, although this study assessed the use of CTP to visually detect positive lacunae based on decreased perfusion and increased delay, no specific measurement or threshold was used.

CONCLUSIONS

This study found that CTP is superior to NCCT/CTA in the detection of acute lacunar infarcts. The specificity was high for lacunar infarct detection by using all of the studied perfusion parameters, but the sensitivity was lower than DWI. CTP is best able to delineate lacunae within the CSWM, followed by the PVWM, but did not accurately identify lacunar strokes within the basal ganglia or thalamus. Further work is necessary to determine which parameter (eg, TTP, MTT, time-to-maximum) best detects lacunae, and a prospective head-to-head comparison of such parameters might be useful.

Disclosures: Alexander McKinney—RELATED: Provision of Writing Assistance, Medicines, Equipment, or Administrative Support: Vital Images. Comments: provided equipment in 2013 that was used in this study. UNRELATED: Consultancy: Vital Images (a division of Toshiba Medical, Minnetonka, Minnesota). Comments: <5,000 total in 2015–16. Expert Testimony: <50,000 legal consultancy in 2015–16. Pascal Salazar—Employment: Vital Images.

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