Objective Assessment of Spasticity by Pendulum Test: A Systematic Review on Methods of Implementation and Outcome Measures

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Abstract

Background: Instrumented pendulum test is an objective and repeatable biomechanical method of assessment for spasticity. However, multitude of sensor technologies and plenty of suggested outcome measures, confuse those interested in implementing this method in practice. Lack of a standard agreement on the definition of outcome measures adds to this ambiguity. In this systematic review of studies, we aim to reduce the confusion by providing pros and cons of the available choices, and also by standardizing the definitions.

Methods: A literature search was conducted for the period of 1950 to the end of 2019 on PubMed, Science Direct, Google Scholar and IEEE explore; with keywords of “pendulum test” and “Spasticity”.

Results: Twenty-eight studies with instrumented pendulum test for assessment of spasticity met the inclusion criteria. All the suggested methods of implementation were compared and advantages and disadvantages were provided for each sensor technology. An exhaustive list categorized outcome measures in three groups of angle-based, angular velocity-based, and angular acceleration-based measures with all different names and definitions.

Conclusions: From a critical point of view, sources of ambiguity were found and explained with the help of graphical representation of pendulum movement stages and corresponding parameters on the angular waveforms. We hope using the provided tables simplify the choices when implementing pendulum test for spasticity evaluation, improve the consistency when reporting the results, and disambiguate inconsistency in the literature.

1. Background

Spasticity according to European Thematic Network to Develop Standardized Measures of Spasticity is “disordered sensory-motor control, resulting from an upper motor neuron lesion, presenting as intermittent or sustained involuntary activation of muscles” [1]. This complex motor disorder which is caused by diverse sources of upper motor neuron lesions, affects patients with stroke[2], spinal cord injury [3], traumatic brain injury[4], multiple sclerosis[5] and cerebral palsy[6]. Spasticity can create severe pain and hence may negatively affect the quality of life. Spasticity can interfere with movement and can lead to stiff, painful joints[7, 8]. This disorder affects more than 12 million persons in the world and interferes with the natural movements of the patients[9, 10]. Billions of dollars are spent in pharmaceutical industry in order to develop anti-spasticity drugs, though lack of repeatable and objective outcome measures hinders the success[8]. It is generally agreed that spasticity is easy to recognize, but not so easy to quantify. Quantitative assessment of spasticity and spasms is crucial in evaluating treatment interventions. Although quantitative clinical scales have been proposed and are currently in use[11–14], but they lack objectivity.

To overcome objectivity issue, one of the promising methods that was introduced about 70 years ago was pendulum test[15]. However, such objective quantification systems that can be easily used in clinics
are still missing. Many attempts can be found in the literature that aimed at providing instrumented pendulum test of spasticity[16–18]. Still, when it comes to methods of implementation and choice of outcome measures, the literature is very diverse and at times non-consistent. This makes practical use of the published research difficult, particularly for those who want to actually implement this method. Although Review studies can be found on pendulum test of spasticity, they have mainly focused on psychometric properties of this method[19, 20]. In this article we have exhaustively searched the published scientific literature in order to come up with a clear list of options for practical methods of implementation. We have further tried to disambiguate available choices of outcome measures for pendulum test of spasticity.

2. Methods

2.1. Search strategy

A systematic review was conducted to identify literature published in four international databases between 1950 and the end of 2019: PubMed, Science Direct, Google Scholar and IEEE explore. Science Direct database was available from 1995 and hence was searched from 1995 to 2019. Combining the keywords “pendulum test” and “Spasticity” is defined as the search strategy. No filters were applied on the type of disease, because it was not the focus of study. The search strategy was the same in all databases, with modifications to fit the web interfaces. Figure 1 shows the search strategy and selection process.

2.2. Study selection and eligibility criteria

After excluding duplicates, the selection of studies was carried out in two stages. All the remained articles were screened first by title and abstract, and then by full text for eligibility. At least one of the mentioned sections should include both “pendulum test” and “spasticity”, and also there should be a mention of quantitative/objective assessment, or instrument/sensor, or outcome measure. In other words, pure clinical studies with no quantitative evaluation of spasticity were excluded.

3. Results

3.1. Description of studies

As summarized in Fig. 1, initial search provided 1575 articles. After removing duplicates, 1551 articles remained from which 1456 were excluded because of not being eligible by examining the title and abstract. From the remaining 95 articles, 70 were removed based on full text assessment for eligibility. Three more relevant studies were found through the articles’ references. Therefore, 28 articles met the eligibility criteria and were included in the review (Table 3).
| Author/Year          | joint  | People under study (number of participants) | Main technology                  | Compared to Clinical Scale |
|---------------------|--------|---------------------------------------------|----------------------------------|---------------------------|
| Couvée,1968[32]    | Knee   | Paraplegia(N = 6) Healthy(N = 5)            | Potentiometer                    | NC                        |
| Bajd,1984[33]      | Knee   | SCI(N = 10) Hemiplegics(N = 5)              | Electro goniometer               | NC                        |
| Leslie,1992[34]    | Knee   | MS(N = 14)                                  | Electro goniometer               | AS                        |
| Stillman,1995[18]  | Knee   | Healthy Young, Middle aged, Elderly (N = 77) | Video camera                     | NC                        |
| He,1997[35]        | Knee   | MS(N = 46)                                  | Electro goniometer               | NC                        |
| Kaeser,1998[36]    | Knee   | Healthy (N = 40) Spastic (N = 9)            | Electro goniometer               | AS                        |
| Greenan Fowler, 2000[6] | Knee | CP (N = 30) Healthy (N = 10)                | Electro goniometer               | MAS                       |
| Cavorzin,2001[37]  | Knee   | Spastic (N = 15) Healthy (N = 10)           | Potentiometer                    | AS                        |
| Nordmark,2002[16]  | Knee   | CP(SDR)(N = 20)                             | Electro goniometer               | MAS                       |
| Lin, 2003[38]      | Elbow  | Stroke(N = 11) Healthy (N = 11)             | Electro goniometer               | AS                        |
| Syczewska,2009[27] | Knee   | CP (N = 21) Trauma(N = 6), DS (N = 3)      | Vicon Motion Capture ENG         | NC                        |
| Bohannon,2009[39]  | Knee   | Chronic stroke (N = 8)                      | Polhemus Liberty magnetic position tracking system | AS                        |
| Sterpi, 2013[17]   | Knee   | Severe cerebral lesion (N = 11) healthy (N = 10) | inertial sensor (Accelerometer, Gyroscope, Magnetometer) | MAS                       |
| Tancredo,2013[29]  | Knee   | SCI (N = 11)                                | Accelerometer, Electro goniometer | MAS                       |
| Lemoyne,2013[40]   | Ankle  | Healthy(N = 1)                              | Accelerometer(IPhone wireless)   | NC                        |
| Author/Year            | joint | People under study (number of participants) | Main technology | Compared to Clinical Scale |
|------------------------|-------|---------------------------------------------|----------------|---------------------------|
| Azevedo,2013 [41]      | Knee  | SCI(N = 5)(5 Time)                          | Electro goniometer | NC                        |
| Szopa,2014 [42]        | Knee  | CP(N = 36)                                   | Accelerometer    | DAROM                     |
|                        |       | Healthy (N = 18)                             |                 |                           |
| Yeh,2016 [43]          | Knee  | Stroke (N = 13)                              | Electro goniometer (Two) | MAS                      |
|                        |       | Healthy (N = 3)                              | Gyroscope (Wii remote) |                           |
| Vargas Luna,2016 [44]  | Knee  | SCI(N = 4)                                   | Goniometer       | AIS                       |
|                        |       |                                            | Video tracking   |                           |
| Bui,2017 [45]          | Knee  | ARSACS (N = 13)                              | Gyroscope        | MAS                       |
|                        |       | Healthy (N = 32)                             | Accelerometer    |                           |
| Popovic-Maneski,2017 [46] | Knee | Chronic SCI(N = 2)                          | Accelerometers (two) | MAS                      |
|                        |       | Healthy(N = 5)                               | Gyroscope        |                           |
|                        |       |                                            | Encoder (Hall-effect) |                           |
|                        |       |                                            | EMG             |                           |
| Popovic-Maneski,2018 [47] | Knee | SCI(N = 9)                                  | Absolute joint angle encoder | AS                      |
|                        |       | Healthy(N = 6)                               | Gyroscope        |                           |
|                        |       |                                            | EMG Electrode    |                           |
| Aleksić,2018 [47]      | Knee  | SCI (n = 1)                                  | Marker-based system | NC                      |
|                        |       | Healthy(N = 1)                               | Joint angle encoder and IMU |                           |
| Popović,2018 [48]      | Knee  | humans with the central nervous system (CNS) lesion | Accelerometers (two) | AS                      |
|                        |       |                                            | Gyroscope        |                           |
|                        |       |                                            | Encoder (Hall-effect) |                           |
|                        |       |                                            | EMG             |                           |
| Author/Year | joint | People under study (number of participants) | Main technology | Compared to Clinical Scale |
|-------------|-------|------------------------------------------|-----------------|--------------------------|
| Whelan, 2018 [49] | Knee | ABI (N = 45) | Fiber-optic goniometer (FOG) | MAS |
|             |       | MS (N = 14) | EMG electrode | |
|             |       | CP (N = 12) | |
|             |       | SCI (N = 22) | |

### 3.2. Assessment of spasticity

Methods of assessment of spasticity can be broadly categorized into clinical, biomechanical, and electrophysiological[21] methods. Clinical methods, that are gold standards in clinic routines, are semi-qualitative. Although clinical scales have been proposed to provide quantitative outcomes, they suffer from lack of objectivity. Biomechanical and electrophysiological methods involve sensors or instruments and can provide objective outcome measures.

A handful of clinical measures such as (CSI: composite spasticity index[22], HAT: hypertonia assessment tool[23], and TSS: triple spasticity scale[24], etc.) have been proposed and used in clinical assessments. However, the most routine method of assessment of spasticity by clinicians are the following four scales that are compared in detail in Table 1, Table 2: Ashworth Scale (AS)[11], Modified Ashworth Scale (MAS) [12], Tardieu Scale (TS)[13], and Modified Tardieu Scale (MTS)[14].

#### Table 2
Comparison of Tardieu and Modified Tardieu scales

| Score | TS[13] | Changed in: MTS[14] |
|-------|--------|---------------------|
| 0     | No resistance throughout the course of the passive movement | No change |
| 1     | Slight resistance throughout the course of passive movement | No Change |
| 2     | Clear catch at precise angle, interrupting the passive movement, followed by release | No Change |
| 3     | Unsustained clonus (less than 10 sec when maintaining the pressure) occurring at a precise angle, followed by release | No Change |
| 4     | Sustained clonus (more than 10 sec when maintaining the pressure) occurring at a precise angle, followed by release | No Change |
| 5     | Joint is immovable | No Change |

All these scales assess spasticity by manual estimation of increased resistance of specific muscle groups to passive motion. From historical point of view, in 1954 Tardieu et al. introduced a 6-point scale to assess spasticity for the first time which was speed dependent.
A decade after that and independently, in 1964, Ashworth proposed a 5-point scale which did not take the velocity dependence of spasticity into account. This scale was modified in 1987 by Bohannon and Smith to deal with the accumulation of most of the scores towards the lower end of the scale. They performed this by including an extra category (1+, Table 1), making it a 6-point scale, and also modified the definitions slightly. In 1999, Boyd and Graham tried to standardize procedure of spasticity assessment and provided the modified TS (kept the 6-point system). MTS quantifies two angles: angle of ‘catch’ (stretch reflex threshold, measured at high speed) and the full range of motion (ROM, an angle measured at low speed). The difference between the two angles is suggested to be an indication of dynamic spasticity (dynamic tone).

### Table 1
Comparison of Ashworth and Modified Ashworth scales

| Score | AS\[11\] | Changed in:\[12\] |
|-------|----------|------------------|
| 0     | No increase in tone | No change |
| 1     | Slight increase in tone manifested by a “catch” when the limb is moved in flexion/extension | Slight increase in tone manifested by a catch, release or minimal resistance at the end of range of motion (ROM) when the limb is moved in flexion/extension |
| 1+    | Slight increase in tone manifested by a catch, followed by minimal resistance throughout the remainder (less than half) of ROM |
| 2     | More marked increase in tone, but the limb is easily moved through its full ROM | More marked increased in tone through most of the ROM, but limb is easily moved |
| 3     | Considerable increase in tone - passive movement difficult | No Change |
| 4     | Limb rigid in flexion and extension | No Change |

Table 1 compares clinical evaluation and scores of spasticity by Ashworth and modified Ashworth scales. Table 2 demonstrates the method of clinical evaluation of spasticity by both Tardieu and modified Tardieu scales. The differences are only in performing the test and interpretation of the results. For passive stretch in MTS only two speeds are utilized. At slow speed, passive range of motion is found as an angle; and at fast speed, spastic reaction is evaluated as another angle. The difference between these two angles is the true measure of dynamic spasticity.

Objective and quantitative assessment methods make evaluation independent of individual judgement and often increase the sensitivity. They resolve the issues of inter- and intra-rater variability as well. From objective and quantitative methods of spasticity assessment, in this review, we focus on one of the most popular biomechanical methods which is pendulum test.

### 3.3. Pendulum test
Introduced in 1951 Wartenberg's pendulum test was designed to objectively assess knee spasticity in a free oscillation when the leg is first raised to horizontal position and then dropped[15]. This test is subjective, simple and quick to implement, reproducible, non-invasive, and is non-intimidating to the children or individuals with cognitive impairments. However, it has its own shortcomings. For example, the results are completely affected by the level of relaxation and by the form of sitting. This test was initially aimed explicitly at the lower limb, but modified versions were later used for upper extremities as well. Boczko et al.[25] modified it in 1958 as an instrumented test with a flashlight and camera to capture the trace of oscillation. Later, many sensor technologies have been used in instrumented pendulum test (Table 4). The common procedure to perform this test starts with the participant sitting in a relaxed position and the leg to test hanging freely over the edge of a seat or a table (Fig. 2). Then the examiner lifts the leg to a horizontal position and lets it swing freely. From this free oscillation, many measures can be extracted to quantify the level of spasticity. Since the test accuracy depends completely on the relaxation of the leg being tested (no voluntary muscle contraction), methods of confirmation of relaxation have been proposed. The two common methods are using Electromyography (EMG)[6, 9], and using phase plane diagram of angle versus angular velocity[26]. Numerous studies have reported the validity and repeatability of this biomechanical test in diverse groups of patients[10, 17, 27].
Table 4
Summary of the popular Technologies used in objective pendulum test, and their advantages and shortcomings

| Technology                          | Advantage                                                                                           | Disadvantage                                                                                     |
|-------------------------------------|-----------------------------------------------------------------------------------------------------|--------------------------------------------------------------------------------------------------|
| Potentiometer (Angle)               | Simple, low cost and suitable for online computer analysis[33].                                      | Higher errors; lower stability; difficult to attach & hindering knee-joint motion[28]              |
|                                     |                                                                                                     | Need for differentiation to get angular velocity / acceleration[51]                                |
| Goniometer (Angle)                  | Easy to attach[51]                                                                                   | Questionable reliability, cause of high individual errors[52]                                      |
|                                     |                                                                                                     | Errors of joint repositioning[53]                                                                    |
| Electrogoniometer (Angle)           | High reliability[51]                                                                                   | Large non-linearity and hysteresis[51]                                                               |
| Accelerometer (Linear acceleration) | Stable and easy to attach. high sensitivity and excellent reliability of the pendulum test[42]   | Less accurate angle estimation during movement[53]                                                   |
|                                     | less expensive; not restricting the movement[51]                                                       |                                                                                                |
| Gyro (Angular velocity)             | No need for numerical differentiation; sufficient accuracy; low susceptibility to effects from the motion of the knee joint axis; no restriction of the knee joint when worn; simple and stable attached; and ability to obtain waveforms of angle, angular velocity, and angular acceleration simply and with high accuracy[51] | Stability and reliability remain problematic[51]                                                   |
| Inertial Motion Units (IMUs, Acceleration plus angular velocity) | Simple use                                                                                          | Issues concerning the validity and reliability of the measurements                               |
| Camera-based methods                | Simple use                                                                                          | Difficult video analysis                                                                          |

Searching the literature for suggestion of hardware or technologies to implement this test, and also for the chosen/best metric that gives enough sensitivity out of this test was not readily available. So in this
review, we have tried to provide a complete list of all possible and clinic-friendly technologies for implementation of this test along with their main advantages and drawbacks. We have also tried to come up with a comprehensive list of outcome measures.

3.4. Methods of implementation of pendulum test

Since its introduction in 1951, the pendulum test was implemented using various devices or technologies, and in different groups of patients with spasticity. However, it took seven years until the first objective data collection was performed by Boczko and Mumenthaler using a battery-fed light and a video camera[28]. Most of the studies have focused on the spasticity at the knee joint, and a few tried to examine spasticity with pendulum test at elbow or ankle joints. In more than half a century, researchers have used this test in objective assessment of spasticity in many diseases including Stroke, Multiple Sclerosis (MS), Cerebral Palsy (CP), Spinal Cord Injury (SCI), lesions (cerebral or in central nervous system), paraplegia and hemiplegia, and trauma. Some of the studies compared healthy participants with their patient population. Almost half of these studies also used clinical scales either to choose the range of spasticity in their patient population[16, 29] or to compare their outcome measures according to the divisions that clinical scales provided[6, 17]. Table 3 presents available studies that used pendulum test in chronological order, indicating the joint under study, participant groups, main technology for implementation of the test, and whether clinical scales are used in the study. There have been important theoretical studies such that Jikuya et al.[30] that have modeled spasticity during the pendulum test, or Kusuhara et al.[28] and Yamamoto et al.[31] that have theoretically examined advantages of using two linear accelerometers in pendulum test, but not included in the table because of no experimental data on patient population.

4. Discussion

4.1. Technologies used in objective pendulum test

Since the method of assessment of spasticity through pendulum test, and the processing steps to reach to the outcome measures are fully dependent on the implemented technology, this aspect is separately assessed in the literature. As Table 3 shows, variety of technologies, from ultrasound sensors[36] to camera-based[27, 50]or fiber-optic goniometers[49], have been used in the devices that implemented the test. However, some of these technologies are used more frequently whose advantages and disadvantages are compared in Table 4.

4.2. Outcome measures of pendulum test

Alongside development of technologies of implementation for pendulum test, numerous measures were suggested to classify the severity of spasticity as outcome measures. Wartenberg used the test qualitatively paying attention to irregularities in swinging time or the number of oscillations. suggested Resting position as his method’s outcome measure. After that, many measures were introduced that are summarized in Table 5.
Table 5
Main categories of outcome measures (parameters) that are suggested in the studies that used pendulum test

| Signal | Category | Parameter | Measure/Parameter Definition | Ref. |
|--------|----------|-----------|-------------------------------|------|
| Angle  | 1        | Onset Ang | Angle at the start of test response | [18] |
|        |          | A0        | Knee angle at the beginning of the test during maximal limb extension | [13, 38, 50] |
|        |          | α         | Initial Knee angle | [44] |
|        |          | Initial angle |               |      |
|        | 2        | F1 Ang    | Angle at the end of initial movement into flexion | [18, 49] |
|        |          | F1 Amp    | F1 Ang – Onset Ang | [18, 49] |
|        |          | Ex        | First swing excursion: the difference between the starting angle (the position at which the examiner released the participant's heel) and the first angle of reversal of the swinging limb | [53] |
|        |          | P4        | First maximum of the oscillation | [33, 43] |
|        |          | FAR       | Knee angle when shank motion first switched from flexion to extension | [17] |
|        |          | A1        | The amplitude of the first swing  
Magnitude of first drop | [33, 35] |
|        |          | ϕ_max     | The first maximum of the goniogram after releasing the leg. | [50] |
|        |          | θ₁        | The peak angle of the first swing | [44] |
|        |          | First reversal |                      |      |
|        | 3        | E1 Ang    | Angle at the end of initial movement into extension | [33] |
|        |          | E1 Amp    | E1 Ang – E1 Ang | [33] |
|        |          | A2        | The angular change between the first minimum and second maximum | [45, 50] |
| Signal | Category | Parameter               | Measure/Parameter Definition                                                                 | Ref.          |
|--------|----------|-------------------------|-----------------------------------------------------------------------------------------------|---------------|
| 4      | Rest     | Rest Ang (RA)           | Resting knee angle                                                                           | [17, 6, 18, 35, 39] |
|        |          | θr                      | Knee angle at the end of oscillations.                                                        |               |
|        |          | Plat Amp                | Rest Ang – onset Ang                                                                          | [18, 49]      |
|        | Frequency| αf                      | Final position of the leg                                                                     | [44]          |
| 5      | Duration | T                       | Duration of oscillations.                                                                     | [6, 42]       |
|        |          | Relative Swing Time     | The time between the peaks, Normalized to the height of the person                           | [16, 27]      |
|        |          | TFR                     | Time to first reversal: time interval between the start of shank motion and the first reversal from flexion to extension. | [17]          |
|        | Test     | Test Duration           | Duration from onset Angle to rest angle                                                       | [18]          |
| 6      | F        | Frequency               | Frequency of oscillations                                                                     | [35, 50]      |
|        |          | C1 Freq                 | Initial cycle frequency = 1/duration of E1 Ang                                               | [18]          |
|        |          | N                       | The number of sinusoidal waves produced by the swinging limb after the heel was released (minimum of 3 degrees) | [6, 33, 46, 48] |
|        |          | P2                      | The Number of swings                                                                          |               |
|        |          | Ncyc                    | Number of cycles (full oscillations) was counted between start of motion and until the oscillation amplitudes is less than 3 degrees. | [39]          |
| 7      | RI       | RI                      | Relaxation index: (starting angle – first angle) / (starting angle – resting angle)          | [26, 43, 48]  |
|        |          | F1 Amp / Plat Amp        |                                                                                               | [18]          |
|        |          | θ1 / θr                 |                                                                                               | [6]           |
|        |          | ERI                     | Extension Relaxation index = E1 Amp / Plat Amp                                                 | [18, 49]      |
| Signal | Category | Parameter | Measure/Parameter Definition | Ref. |
|--------|----------|-----------|------------------------------|------|
| β      | Damping ratio. Defined as the ratio of the logarithmic decrement (δ) to the period; expressed in sec | [42] |
| λ      | Defined as the natural log of the second to fourth peak amplitude ratio | [42] |
| P1     | Normalized relaxation index | [33, 43] |
| P5     | Relaxation index at the half swing | [33, 43] |
| P6     | Average relaxation index of 10 successive swings | [33] |
| Ratio 1 | Ratio 1: A1/(A1 – A2), where A1 is the amplitude of the first oscillation and A2 is the amplitude of the second oscillation. | [17, 26, 32, 33, 52] |
| Ratio R1 | Ratio R1: A/B, where A is the amplitude of the first oscillation and B is the amplitude of the second oscillation. | [17, 26, 32, 33, 52] |
| R1 ratio | The amplitude of the first swing (A) divided by the amplitude of the rebound angle. | [17, 26, 32, 33, 52] |
| Ratio 2 | Ratio 2: A1/A0, where A0 is the final resting angle and A1 is the amplitude of the first oscillation. | [33, 34, 36, 16, 27, 45] |
| Ratio R2 | R2: first swing (A) divided by the amplitude of the final position (C). | [33, 34, 36, 16, 27, 45] |
| R2 ratio | | |
| R2n    | The normalized relaxation index. R2n: A1/1.6A0 where A0 is the knee angle between the full extension (starting position) and the neutral knee joint angle (end position), and A1 is the difference between the starting angle and the maximum flexion | [33, 44, 50] |
| 8      | AUC      | Area Under Curve: area between the knee angle during oscillations and the resting angle; it is the integral of the absolute value of the knee angle | [17, 39] [33] |
| P3     | The area between the goniogram and the time axis. | [50] |
| Ptotal | Relative area difference | [50] |
|        | Relative difference | |
| Signal | Category   | Parameter | Measure/Parameter Definition                                                                 | Ref.  |
|-------|------------|-----------|------------------------------------------------------------------------------------------------|-------|
| 9     | PT         | Total pendulum Score (combination of multiple parameters)                                      | [50]  |
|       |            |           |                                                                                               |       |
|       | Angular Velocity | ωmax      | The maximum angular velocity of the shank                                                      | [50]  |
|       |            | Vmax      | maximal velocity of the first swing (°/s)                                                       | [16, |
|       |            |           |                                                                                                | 26,  |
|       |            | F1 Vel    | Maximum velocity during F1 Amp                                                                 | [18]  |
|       |            | P7        | First maximum of the tachogram                                                                | [33]  |
| 2     | VFR        | Velocity to first reversal:                                                                    | [17, |
|       |            |           | VFR = FAR /TFR                                                                                  | 39]   |
| 3     | E1 Vel     | Maximum velocity during E1 Amp                                                                 | [18]  |
|       | P8         | First minimum the tachogram                                                                  | [33]  |
|       | ωmin       | The minimum angular velocity of the shank                                                     | [50]  |
|       | Angular Acceleration | F1 A/D ratio | Initial flexion acceleration/deceleration ratio = Max acceleration duration F1 Amp/ Max deceleration during F1 Amp | [18]  |
|       |            | First Maximum Acceleration                                                                    | [26]  |
|       |            | Max Acc on the rebound swing                                                                 | [26]  |

The first mentioned set of outcome measures from pendulum test of spasticity on the knee were by Boczko et al.[25] in 1950s. During the following half a century, other than number of oscillations, test duration and peak angles, other measures such as relaxation index (RI) were introduced to have higher reliability. The most comprehensive works on outcome measures during this time were performed by Bajd et al.[33, 46, 47] and Stillman et al.[18]. Table 5 illustrates all categories of outcome measures that have been suggested in the literature of pendulum test of spasticity. The three main categories are parameters based on angle data, based on angular velocity, and finally based on angular acceleration. All the investigated studies have used outcome measures that are based on joint angle during the test. Almost half of the studies have used parameters that are based on angular data (Table 5). A considerable amount of the studies has used more than one category (Table 5).

Overall, the suggested parameters can be divided into two categories of primary and secondary measures. Primary measures are directly obtained from aspects of the collected data such as the peak
value of an angle, or number of oscillations (for example the first six categories in Table 5 for parameters based on angle data). Secondary outcome measures are calculated or combined from the primary ones mainly to reduce the number of parameters and to come up with ones that are more sensitive or better illustrate level of spasticity.

Outcome measures that are based on angle data are divided into 9 categories in Table 5. Category #1 is based on the initial position of the extended knee in the test. Although 29% of studies (out of 17 that we have investigated) have used this category in their set of parameters, it is not an outcome measure of spasticity test by itself, but is mainly used in the calculation of other outcome measures. Second category is used by 71% of the studies and relies on the maximum flexion angle in the first swing after the leg release. Category #3 examines the max angle in the first rebound towards extension of the knee, which is used by 18% of the studies. Resting angle or the final position of the leg is category #4 and is used by 41% of the literature. Category #5 examines durations in the test, whether overall duration or the time between two specific points, and is used by 35% of the studies. Number of cycles or frequency is category #6 and is used by 59% investigators. In counting the oscillations, a threshold of three degrees is considered below which the oscillations are ignored. Frequency concept was either used as the inverse of the time duration for the first cycle, or as the ratio of the number of total cycles to the total time. Time and frequency categories could be based on angular velocity or acceleration during the test, but almost all the researchers have based them on the angle data. Categories #7–9 are secondary measures and are calculated from the previous categories. Category #7 examines the ratio of the amplitudes for various angles. Wide range of ratios have been suggested by researchers and almost all studies (94%) have used at least one such category of outcome measure. Most of the powerful and consistent outcome measure that were capable of identifying levels of spasticity were in this category\[44, 45\]. Category #8 uses area under the knee angle curve which considers positive and negative values for flexion and extension around the resting angle, and is used by 24% of the studies. Recently, Popovic et al. suggested a total score for pendulum test which takes many aspects of the angle curve into account and comes up with a final score\[50\]. This is category #9 in Table 5.

There are three categories of outcome measures in the angular velocity group. Category #1 uses the first maximum angular velocity in the flexion direction, and is used by 35% of the investigators. Category #2 relies on the average angular velocity in the first swing towards the flexion, and is used by 12% of the literature. Category #3 is based on the first maximum velocity in the rebound towards the knee extension, and is suggested by the 18% of the literature. Some of the researchers call this category the minimum velocity instead of maximum velocity in the opposite direction.

Few studies have used outcome metrics that rely on angular acceleration. Stillman et al.\[18\] suggested the ratio of maximum acceleration to maximum deceleration during the first swing towards flexion of the knee as their measure of spasticity. Maximum angular acceleration both in flexion and in extension phases are separately used as outcome measures by Brown et al.\[26\] in 1988.
As can be seen from the table, quite a lot of parameters have been suggested as outcome measures. However, it is not practical to use all of the suggested parameters, and unfortunately no study has compared all these parameters to provide a comprehensive subjective scale of strength/weakness points. Nonetheless, some of the studies have chosen reasonable number of outcome measure (and some provided a rationale for their choice). Table 6 is the list of the main studies on the outcome measures of pendulum test that is used in this review.

### Table 6
Sets of outcome measures that were proposed in each key study

| # of used parameters | List of Parameters (Measures)                                                                 | First author            |
|----------------------|---------------------------------------------------------------------------------------------|-------------------------|
| 8                    | p1-p8 (using A0, A1, A2, R1,R2,R2n)                                                        | Bajd [33]               |
| 6                    | Ex, RI, β, λ, t, n                                                                        | Szopa [42]              |
| 4                    | p1, p2, p4, p5                                                                           | Yeh [43]                |
| 1                    | R2n index (using αf, αs, αp)                                                              | Vargas Luna [44]        |
| 4                    | RI, Test duration, Fang, Rest ang                                                         | Azevedo [41]            |
| 2                    | Ratio 1 & Ratio 2                                                                         | Bui [45]                |
| 1                    | PT score                                                                                  | Popovic-Maneski [50]    |
| 2                    | Ratio R1, Ratio R2                                                                       | Leslie [34]             |
| 5                    | Θ1, N, Duration, RI, θr                                                                   | Greenan Fowler [6]      |
| 4                    | R2 ratio, R1 ratio, Vmax, Relative swing time                                             | Nordmark [16]           |
| 4                    | First Reversal, AUC, VFR, Resting Angle                                                  | Bohannon [39]           |
| 5                    | FAR, IA, AUC, TFR, VFR                                                                   | Sterpi [17]             |
| 14                   | On Ang, Rest Ang, F1 Ang, E1 Ang, F1 Amp, E1 Amp, plat Amp, RI, ERI, F1 Vel, E1 Vel, F1 A/D ratio, Duration, C1 Freq | Stillman [18]           |
| 5                    | F1 Amp, E1 Amp, plat Amp, RI, ERI                                                         | Tancredo [29]           |
| 4                    | RI, Vmax, First Maximum Acceleration, Max Acc on the rebound swing                        | Brown [26]              |
| 3                    | A0, A1, Resting Angle                                                                    | He [35]                 |
| 6                    | RI, ERI, F1 Amp, E1 Amp, Plat, Ncyc                                                       | Whelan [49]             |

In the literature of the pendulum test for spasticity, there is no standard agreement between the researchers particularly in definition of the outcome measures. One main reason for this ambiguity is the
different references used for measuring the knee angle. Overall, four key positions can be used as a reference: Horizontal plane, vertical plane, initial shank position, and final shank position in the test. Figure 3-a shows these four possible frames of reference for knee angle, along the first four categories of angle parameters in Table 5.

Most of the studies have used horizontal plane as their frame of reference[6, 16–18, 26, 29, 34, 42]. The second most popular frame of reference for angular movement is rest angle or the final position of the knee in the pendulum test[27, 33, 35, 36, 43, 50]. Some of the researchers have used the initial angle of the shank as their reference instead of horizontal plane[39, 45, 49]. No researcher has used vertical plane as their reference in knee angle measurement. One example of such ambiguity is A0 which depending on the reference is defined as “Final resting angle” [45] as well as “knee angle at the beginning of the test during maximal limb extension” [17, 35]. Similarly, differences can be observed in the definition of other spasticity measures such is definition of RI in[6, 18] and in[33, 43].

Figures 3-b illustrate two typical knee angle traces during a pendulum test. The bold trace corresponds to when the reference is the resting angle. Sections of knee angle trace, that parameters (angle outcome measures) in categories #1-#4 are extracted, are marked. The dotted trace corresponds to when the reference is horizontal plane. If the beginning of trace falls on the time axis, then the reference is initial angle.

5. Conclusions

This systematic review aimed at analyzing the state of the art in implementation of Pendulum test and the outcome measures of this method of evaluation of spasticity. This test is agreed to be repeatable and a valid method of identifying presence of spasticity[27, 39], though it may not be successful in discriminating between close levels of spasticity[49]. Since lower leg weight is suitable to create enough speed through free fall in the pendulum test, which is crucial for this speed dependent symptom, most of this test’s applications is on the knee joint. However, using extra weight and special apparatus, this test can be applied to other joints such as elbow[38].

Non-instrumented pendulum test lacks objectivity and is apparently not used much by researchers. Instrumented pendulum test using multitudes of sensor technologies have been reported in the literature and evaluated as a feasible method of objective assessment of spasticity particularly for the knee extensors[18, 54, 55].

Sensor technologies that are used for implementation of this test (Tables 1, 2) would affect reliability/repeatability, ease and speed of setup, size and hindrance to pendular movement and hence suitability for clinical use, susceptibility to interfering factors such as gravity, ease of data processing and analysis and hence possibility of implementation in stand-alone devices. Overall, in the past few decades, the most technology been used is goniometer and electro-goniometer. Choice of sensor affects the type of signal that is used in data collection and thereby in outcome measure for the test. Although, processing techniques such as differentiation can transform angle data to angular velocity or
acceleration. As can be seen in Table 5, all of the studies that we found to provide objective assessment method of spasticity with outcome metrics, used angular data. Almost half of them have also used angular data whether using tachometer/gyroscopes or differentiating angular data. Finally, almost 10% of the studies have focused on angular acceleration data as well.

We have categorized all 33 outcome measures that appeared in the literature into 13 categories in Table 5. These measures/metrics are supposed to help pendulum test differentiate between healthy and various levels of spasticity in the joint under consideration. Some of the studies have commented on the sensitivity of single outcome measures[6, 49, 56]. Each of the studies we investigated utilized between one to 14 outcome measures (Table 6).

Most of the studies have used more than one measure and argue that no single measure can represent all abnormal aspects of passive resistance of the disordered joint to the movement[18]. Unfortunately, there has been no study that optimizes a model using all or some of these 33 measures and comes up with a single combined measure with the highest discriminative power. Although such a model might be different for various spastic groups of patients. Nonetheless, some of the studies have tried such modeling approach without doing the optimization step. For example, Whelan et al. tried two models to find presence of knee spasticity in four different patient cohorts[49]. Another example is the attempt by popovic-Maneski et al.[50] in providing a single measure called global measure of spasticity.

Finally, such metrics that come out of pendulum test is supposed to be used by clinicians and should prove its power in a comparison by their golden clinical measures. Out of 5 clinical scales that are mentioned in studies we investigated, MAS and AS were the mostly used ones (Table 3). However, a modeling study that provides a relationship between such clinical scale as a gold standard and a single/combined outcome measure is really missing.

In this review we tried to come up with a comprehensive list of outcome measures along with the suggested sets of measures by lead researchers in this field (Table 5–6). We tried to provide standardized definitions for outcome measures through 13 categories for three type of signals (Table 5). However, it seems that a thorough modeling study is still missing. One that tries to take all of the 33 outcome measures into account and provides the best minimal sets of necessary parameters. Such final model, if provided, will accelerate making acceptable clinical device for objective assessment of spasticity.

**Abbreviations**

CSI: Composite Spasticity Index; HAT:Hypertonia Assessment Tool; TSS:triple Spasticity Scale; AS: Ashworth Scale; MAS:Modified Ashworth Scale; TS:Tardieu Scale; MTS:Modified Tardieu Scale; ROM:Range Of Motion; MS:Multiple Sclerosis; CP:Cerebral Palsy; SCI:Spinal Cord Injury; RI:Relaxation Index; NC:No Comparison; CP:Cerebral Palsy; MS:Multiple Sclerosis; SCI:Spinal Cord Injury; DS:Degenerative Syndromes of the nervous system; NR:Not report in original paper; PTD:Pendular Test Device; DAROM:Dynamic Evaluation of Range of Motion scale; AIS:Association Impairment Scale; ARSACS:Autosomal Recessive Spastic Ataxia of Charlevoix/Saguenay; IMU:Inertial measurement Units;
Declarations

Ethics approval and consent to participate

Not applicable.

Consent for publication

Not applicable.

Availability of data and materials

The generated or analyzed data during this study are all included in the published article.

Competing interests

The authors declare that they have no competing interests.

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Author's contributions

FR and RE conceived the work and designed the article. RE and NS performed the literature review. FR and RE wrote and revised the manuscript. FR, MRA, and NS edited the manuscript. FR supervised the work. All authors read and approved the final manuscript.

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Figures
Figure 1

Flow chart of the search and selection process of the systematic review of Objective assessment of spasticity by pendulum test for methods of implementation and outcome measures
Figure 2

Experimental setup for pendulum test of spasticity at the knee level
Figure 3

a) The first couple of swing traces along the first four category of outcome measures (#1-#4) that are key joint angles during the pendulum test and explained in Table 5. b) Time series for the knee joint angle during the pendulum test along the first four category of outcome measures. The bold trace corresponds to when the reference is the resting angle. The dotted trace corresponds to when the reference is horizontal plane.