Cementless total hip arthroplasty for primary osteoarthritis in patients aged 55 years and older

Results of the 8 most common cementless designs compared to cemented reference implants in the Finnish Arthroplasty Register

Keijo T Mäkelä¹, Antti Eskelinen², Pekka Paavolainen³, Pekka Pulkkinen⁴, and Ville Remes⁵

¹Department of Orthopaedics and Traumatology, Turku University Central Hospital, Turku; ²Coxa Hospital for Joint Replacement, Tampere; ³Orton Orthopaedic Hospital, Invalid Foundation, Helsinki; ⁴Department of Public Health, University of Helsinki, Finland; ⁵Department of Orthopaedics and Traumatology, Helsinki University Central Hospital, Helsinki, Finland

Correspondence: keijo.makela@tyks.fi
Submitted 09-08-04. Accepted 09-12-04

Results obtained from the Scandinavian arthroplasty registries (Havelin et al. 2000, Puolakka et al. 2001a, Malchau et al. 2002) on a nation-by-nation basis and studies from single centers worldwide (Berry et al. 2002, Wroblewski et al. 2002, Della Valle et al. 2004, Buckwalter et al. 2006, Morshed et al. 2007) have indicated that cemented total hip replacement is the treatment of choice for severe osteoarthritis in elderly patients. We therefore separately analyzed the survival rates of the most common cementless designs performed for primary osteoarthritis in patients aged 55 years or older in Finland, and compared the risk of revision for each implant with that of the cemented implant reference group (Mäkelä et al. 2008b). These analyses were carried out on population-based data obtained from the Finnish Arthroplasty Register for the period 1980 through 2005.

Background
Cemented total hip arthroplasty has been the treatment of choice for elderly patients with osteoarthritis. We analyzed survival rates of the most common cementless designs used in this age group in Finland.

Patients and methods
Inclusion criteria permitted 10,310 replacements (8 designs) performed in patients aged 55 years or older to be selected for evaluation. The risk of revision of each of the 8 implants was compared with that of a group comprising 3 cemented designs as the reference (9,549 replacements). Survival analyses were performed overall and separately for 3 age cohorts: 55–64 years (6,781 replacements), 65–74 years (8,821 replacements), and 75 years or older (4,257 replacements).

Results
In all patients aged 55 years or more, the Bi-Metric stem had a higher survival rate for aseptic loosening at 15 years than the cemented reference group: 96% (95% CI: 94–98) vs. 91% (CI: 90–92). However, the 15-year survival rates of the Bi-Metric/Press-Fit Universal (71% (CI: 67–75)) and the Anatomic Mesh/Harris-Galante II (72% (CI: 67–78)) total hip replacements were lower than that of the reference group (86% (CI: 84–87)). Information was scarce for patients aged 75 years or more.

Interpretation
Cementless proximal porous-coated stems are a good option for elderly patients. Even though biological fixation is a reliable fixation method in THA, polyethylene wear and osteolysis remain a serious problem for cementless cup designs with unplugged screw holes and low-quality liners.

Patients and methods
Since 1980, data on total hip replacements have been collected and archived in the Finnish Arthroplasty Register (Paavolainen et al. 1991, Puolakka et al. 2001a). Healthcare authorities, institutions, and orthopedic units in Finland are obliged to provide the National Agency for Medicines with information that is essential for monitoring past and current trends for the efficacious use of materials, approaches, and designs used in
orthopedics. The coverage in the Finnish Arthroplasty Register was initially analyzed for the period 1994–1995 by comparing its data with those of the discharge registers of participating hospitals; the Register covered 90% of all implantations performed (Puolakka et al. 2001a). Since 1995, the data in the register have been compared with those of hospital discharge registers every few years. Currently, 98% of implantations are recorded in the Finnish Arthroplasty Register (Peltola 2008).

Study population and inclusion criteria

During the study period (1980–2005), 101,720 primary total hip replacements were performed in Finland. Of these, 87,578 (86%) were performed on patients aged 55 years or older. Primary osteoarthritis was the indication in 71,146 (81%) of these operations; cementless total hip implants were used in 30,112 (42%).

Only designs used in more than 500 operations during the study period and with more than 20 hips at risk at 5 years were included in the current study. These criteria permitted the inclusion of 8 designs (10,310 replacements) (Table 1). The risk of revision for each design was compared with that for 9,549 cemented reference implants (Table 2). A 10-year survival rate exceeding 90% is commonly regarded as a good long-term outcome (National Institute of Clinical Excellence, NICE). The 3 best performing cemented designs in Finland (Mäkelä et al. 2008b) fulfilled this criterion and were chosen as

Table 1. Demographic data of the implants analyzed

| THR Brands         | No. | Mean follow-up | Mean age | Women (%) | No. of hospitals | Period of implantation |
|--------------------|-----|----------------|----------|-----------|------------------|------------------------|
| Anatomic Mesh/HG-II | 604 | 11.1           | 63       | 56        | 24               | 1989–1997              |
| PCA Std/PCA Pegged | 508 | 11.6           | 63       | 55        | 23               | 1985–1995              |
| Bi-Metric/PFU      | 2,687 | 8.8           | 63       | 49        | 53               | 1986–2001              |
| Bi-Metric/Mallory  | 637  | 8.7            | 67       | 60        | 11               | 1989–2000              |
| Bi-Metric/Vision   | 2,055 | 3.4           | 65       | 48        | 47               | 1998–2005              |
| ABG I/ABG I        | 556  | 9.1            | 65       | 55        | 25               | 1992–1997              |
| ABG I/ABG II       | 1,765 | 5.9           | 66       | 51        | 36               | 1996–2003              |
| ABG II/ABG II      | 1,489 | 2.5           | 67       | 55        | 31               | 2000–2005              |
| Cemented reference | 9,549 | 8.8           | 72       | 66        | 62               | 1980–2005              |
| Together           | 19,859 | 7.6           | 68       | 59        | 77               | 1980–2005              |

HG-II: Harris-Galante II; PCA Std: porous-coated Anatomic Standard; PFU: Press-Fit Universal; ABG: Anatomique Benoist Girard.

Table 2. Material, surface, design features, and manufacturer of the implants. For abbreviations, see Table 1

| THR Brands          | Material     | Surface                        | Special design features                      | Manufacturer       |
|---------------------|--------------|--------------------------------|-----------------------------------------------|--------------------|
| **Stems**           |              |                                |                                               |                    |
| Bi-Metric           | Titanium alloy | Proximally porous-coated      | Straight, collarless                          | Biomet             |
| Anatomic Mesh       | Titanium alloy | Proximally porous-coated      | Anatomic                                      | Zimmer             |
| ABG I               | Titanium alloy | Proximally grit-blasted and HA-coated | Anatomic                                      | Stryker Howmedica  |
| PCA Standard        | CoCr alloy   | Proximally porous-coated      | Straight, collarless, cemented                | Stryker Howmedica  |
| Exeter Universal    | Stainless steel | Polished          |                                               | Stryker Howmedica  |
| Müller Straight     | CoCr alloy   | Matt                          | Straight, small collar, fluted macrostructure | Zimmer             |
| Lubinus SP II Cups  | CoCr alloy   | Matt                          | Anatomic, collar, modular                     | Link               |
| ABG I               | Titanium alloy | Grit-blasted and HA-coated    | Hemispherical, open screw-holes                | Stryker Howmedica  |
| ABG II              | Titanium alloy | Grit-blasted and HA-coated    | Hemispherical, open screw-holes plugged       | Stryker Howmedica  |
| Biomet Mallory      | Titanium alloy | Porous-coated                 | Hemispherical, open screw-holes, fins         | Biomet             |
| Biomet Universal    | Titanium alloy | Porous-coated                 | Hemispherical, open screw-holes               | Biomet             |
| Biomet Vision       | Titanium alloy | Porous-coated                 | Hemispherical, open screw-holes plugged       | Biomet             |
| Harris-Galante II   | Titanium alloy | Porous-coated                 | Hemispherical, open screw-holes               | Zimmer             |
| PCA Pegged          | Cobalt-chromium | Porous-coated  | Hemispherical, open screw-holes               | Stryker Howmedica  |
| Exeter All-poly     | Polyethylene | –                             | Cemented                                      | Stryker Howmedica  |
| Müller Std          | Polyethylene | –                             | Cemented                                      | Zimmer             |
| Lubinus IP          | Polyethylene | –                             | Groove design                                 | Link               |
reference implants. These 3 cemented designs were the Exeter Universal stem combined with the All-poly cup (Stryker, Mahwah, NJ), the Müller Straight stem combined with the Müller Standard cup (Zimmer, Warsaw, IN), and the Lubinus SP II stem combined with the Lubinus IP cup (Waldemer Link, Hamburg, Germany). Survival analyses were performed for the whole study population and separately for each of 3 age cohorts: 55–64 years, 65–74 years, and 75 years and older. The data from subgroup analysis were massive and only the data with “any reason” as cause of revision are presented (Table 7).

Revisions were linked to the primary operation by using the patient’s personal identification number; these numbers are assigned to every resident of Finland. Numbers and indications for revision were recorded (Table 3).

**Statistics**

The endpoint for survival was defined as revision when any component (including femoral head and liner) or the whole implant was removed or exchanged. Survival rates for stems and cups were analyzed separately with revision for aseptic loosening being used as the endpoint. When survival analyses were conducted for total hip replacements (cup + stem combinations), both revision for any reason and revision for aseptic loosening served as discrete endpoints. Kaplan-Meier survival analysis was used to calculate the survival probabilities of implants at 7, 10, and 15 years. The survival rate of any respective implant was determined only when there were at least 20 hips at risk at the follow-up point (Furnes et al. 2001). Patients who had died or emigrated from Finland during the follow-up period were censored at that point. Survival data obtained by Kaplan-Meier analysis were compared by the log-rank test. The Cox multiple regression model was used to study differences between implants and to adjust for potential confounding factors.

Both Kaplan-Meier and Cox regression are methods based on assumptions of independent observations. However, bilateral observations cannot be regarded as being independent (Robertsson and Ranstam 2003, Bryant et al. 2006). Violation of this independence assumption may have an effect on the validity of the results. To avoid this violation, the data analysis could be performed by allowing inclusion of correlated observations, e.g. including only one prosthesis per patient or by including a shared frailty variable in the Cox regression. In the current study, however, bilateral observations were included in the dataset analyzed. It has been found that the effect of neglecting bilateral prostheses is minute (Havelin et al. 1995, Robertsson and Ranstam 2003, Lie et al. 2004).

**Risk of revision ratios of stems, cups, and total hip replacements (cup + stem combinations) were analyzed. Adjustments were made for age and sex. The 3 best performing cemented designs in Finland were chosen as reference implants (Mäkelä et al. 2008b). The survival data of these cemented designs were combined to form a single reference group. Cox regression analyses provided survival probabilities and adjusted risk ratios for revision. Estimates derived from the Cox analyses were used to construct adjusted survival curves at mean values of the risk factors. The proportional hazards assumption of the Cox model (meaning that the relative difference between revision rates should be constant over time since the primary operation) was not reached.**

| Table 3. Reasons for revision of the 8 most common cementless brands and the cemented reference designs. Percentage in parentheses. For prosthesis types, see Table 1 |
|------------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|
| A THR brand      |                |                |                |                |                |                |                |                |                |                |                |
| B No. of primary operations |                |                |                |                |                |                |                |                |                |                |                |
| C Aseptic loosening (cup + stem) |                |                |                |                |                |                |                |                |                |                |                |
| D Aseptic loosening (cup) |                |                |                |                |                |                |                |                |                |                |                |
| E Aseptic loosening (stem) |                |                |                |                |                |                |                |                |                |                |                |
| F Infection      |                |                |                |                |                |                |                |                |                |                |                |
| G Dislocation    |                |                |                |                |                |                |                |                |                |                |                |
| H Malposition    |                |                |                |                |                |                |                |                |                |                |                |
| I Fracture of the prosthesis |                |                |                |                |                |                |                |                |                |                |                |
| J Periprosthetic fracture |                |                |                |                |                |                |                |                |                |                |                |
| K Any other reason |                |                |                |                |                |                |                |                |                |                |                |
| L Together       |                |                |                |                |                |                |                |                |                |                |                |
| A               | B              | C              | D              | E              | F              | G              | H              | I              | J              | K              | L              |
| Anatomic Mesh/HG-II | 604            | 17 (15)        | 23 (20)        | 17 (15)        | 0 (0)          | 4 (4)          | 7 (6)          | 4 (4)          | 2 (2)          | 39 (35)        | 113             |
| PCA Std/PCA Pegged | 508            | 19 (14)        | 81 (60)        | 19 (14)        | 2 (2)          | 1 (1)          | 2 (2)          | 0 (0)          | 1 (1)          | 10 (7)         | 135             |
| Bi-Metric/PFU    | 2,687          | 26 (8)         | 67 (19)        | 10 (3)         | 9 (3)          | 57 (17)        | 14 (4)         | 16 (5)         | 15 (4)         | 131 (38)       | 345             |
| Bi-Metric/Mallory | 637            | 5 (8)          | 11 (17)        | 3 (5)          | 1 (2)          | 12 (19)        | 3 (5)          | 5 (8)          | 3 (5)          | 21 (33)        | 64              |
| Bi-Metric/Vision | 2,055          | 11 (16)        | 1 (1)          | 6 (9)          | 8 (12)         | 28 (41)        | 5 (7)          | 0 (0)          | 4 (6)          | 6 (9)          | 69              |
| ABG I/ABG I     | 1,765          | 1 (2)          | 6 (10)         | 2 (3)          | 5 (8)          | 13 (21)        | 10 (16)        | 1 (2)          | 10 (16)        | 15 (24)        | 63              |
| ABG II/ABG II   | 1,489          | 2 (4)          | 1 (2)          | 3 (6)          | 3 (6)          | 10 (20)        | 7 (14)         | 4 (8)          | 19 (37)        | 2 (4)          | 51              |
| Cemented reference | 9,549          | 227 (28)       | 142 (18)       | 253 (32)       | 385 (5)        | 73 (9)         | 20 (3)         | 5 (1)          | 24 (3)         | 16 (2)         | 798             |
| Together        | 19,859         | 318 (18)       | 359 (21)       | 316 (18)       | 67 (4)         | 204 (12)       | 71 (4)         | 38 (2)         | 84 (5)         | 287 (17)       | 1,744           |
in some analyses performed. Thus, adjusted risk ratios were also established within time intervals (0–7 years, 7 years after the primary operation). The Wald test was used to calculate the p-values for data obtained from the Cox multiple regression analyses. A difference between groups was considered to be statistically significant if the p-value was less than 0.05 in a two-tailed test.

Results

Survival of stems – aseptic loosening

When all patients aged 55 years or more were analyzed as a single group, the Bi-Metric stem had a higher 15-year survival rate than the reference group (95% (CI: 97–99) vs. 90% (CI: 89–91), respectively). For the age groups 55–64 years and 65–74 years, the Bi-Metric stem had a higher 15-year survival rate than the reference group (95% (CI: 97–99) vs. 84% (CI: 80–87) and 98% (CI: 97–99) vs. 90% (CI: 89–91), respectively).

Survival of cups – aseptic loosening

When all patients aged 55 years or more were analyzed as a single group, the survival of the PCA Pegged cup at 15 years was lower than that of the reference group. Apart from this exception, there were no differences in survival rates between cementless cups and that of the reference group at 15-years. The Cox regression analysis revealed that the PCA Pegged cup had a significantly increased risk of revision both during the first 7 years postoperatively and beyond 7 years of follow-up. Furthermore, during the first 7 years the Press-Fit Universal, the Mallory, the Vision, and the ABG II cups had significantly reduced risks of revision compared to the reference group (Table 5). Beyond 7 years of follow-up, however, the lower revision risk remained only for the Press-Fit Universal cup (Table 5, Figure 1B). The number of Vision and ABG II cups for analysis beyond 7 years was low (Table 5).

Table 4. Survival of cementless stems and the cemented reference group. Endpoint was defined as revision due to aseptic loosening of the stem. 7-, 10-, and 15-year survival rates were obtained from the Kaplan-Meier analysis. For prosthesis types, see Table 1

| A          | B        | C     | D     | E     | F     | G     | H     | I     | J     | K     | L     |
|------------|----------|-------|-------|-------|-------|-------|-------|-------|-------|-------|-------|-------|
| All (≥ 55 years) |          |       |       |       |       |       |       |       |       |       |       |       |
| Anatomic Mesh |          |       |       |       |       |       |       |       |       |       |       |       |
| FU ≤ 7 years | 604      | 11.1  | 532   | 98    | (97–99)| 444   | 96    | (94–98)| 91    | 92    | (89–95)| 0.53   | (0.37–0.76)| 0.001  |
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 0.38  | (0.21–0.71)| 0.002  |
| PCA Std     |          |       |       |       |       |       |       |       |       |       |       | 0.64  | (0.40–1.00)| 0.05   |
| FU ≤ 7 years | 508      | 11.6  | 430   | 98    | (96–99)| 351   | 95    | (92–97)| 146   | 89    | (86–93)| 0.62  | (0.44–0.88)| 0.007  |
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 0.49  | (0.27–0.89)| 0.02   |
| Bi-Metric   |          |       |       |       |       |       |       |       |       |       |       | 0.68  | (0.44–1.05)| 0.08   |
| FU ≤ 7 years | 5,379    | 6.8   | 2,698 | 99    | (99–99)| 1,463 | 98    | (98–99)| 154   | 96    | (94–98)| 0.18  | (0.12–0.26)| < 0.001|
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 0.20  | (0.15–0.27)| < 0.001|
| ABG I       |          |       |       |       |       |       |       |       |       |       |       | 0.08  | (0.04–0.18)| < 0.001|
| FU ≤ 7 years | 2,330    | 6.7   | 1,152 | 100   | (99–100)| 342   | 98    | (97–99)| 0     | –     |       | 0.15  | (0.09–0.25)| < 0.001|
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 0.00  | (0.00–0.45)| 0.009  |
| ABG II      |          |       |       |       |       |       |       |       |       |       |       | 0.40  | (0.20–0.80)| 0.009  |
| FU ≤ 7 years | 1,489    | 2.5   | 0     | –     |       | 0     | –     |       | 0     | –     |       | 0.31  | (0.13–0.76)| 0.01   |
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 0.31  | (0.13–0.76)| 0.01   |
| Cemented    |          |       |       |       |       |       |       |       |       |       |       | 1.0   | (reference)| –      |
| FU ≤ 7 years | 9,549    | 8.8   | 6,231 | 97    | (96–97)| 4,442 | 95    | (94–95)| 1,115 | 91    | (90–92)| 1.0   | (reference)| –      |
| FU > 7 years |          |       |       |       |       |       |       |       |       |       |       | 1.0   | (reference)| –      |
| Total       | 19,859   |       |       |       |       |       |       |       |       |       |       | 1.0   | (reference)| –      |

A Age group
B Brand of stem
C Number of operations
D Mean follow-up (in years)
E At risk (7-year)
F % 7-year survival (95% CI)
G At risk (10-year)
H % 10-year survival (95% CI)
I At risk (15-year)
J % 15-year survival (95% CI)
K Adjusted RR* for revision (95% CI)
L p-value

*RR: risk ratio from the Cox regression analysis (other stem brands compared to the cemented reference stems, with adjustment made for age and sex)
For patients aged 55–64 years, the HG-II cup (87% (CI: 82–91)) and the PFU cup (88% (CI: 84–93)) had similar survival rates at 15 years as the reference cups (85% (CI: 81–88)). For patients aged 65–74 years, the PFU cup had higher survival rate at 15 years than the reference group (96% (CI: 94–98) vs. 92% (CI: 91–93)).
Survival of total hip replacements (cup + stem combinations) – aseptic loosening

When all patients aged 55 years or more were analyzed as a single group, the 15-year survival of the PCA Standard/PCA Pegged was lower than that of the reference group. The Cox regression analysis revealed that the PCA Standard/PCA Pegged had a significantly increased risk of revision beyond 7 years of follow-up. In contrast, all other cementless cup designs showed lower risk of revision than the cemented reference group during the first 7 years, and the Bi-Metric/Press-Fit Universal, the Bi-Metric/Mallory, and the ABG I/ABG II even beyond 7 years (Figure 2A, Table 6). Beyond 7 years, the number of Bi-Metric/Vision THRs was low (Table 6).

For patients aged 55–64 years, the 15-year survival rate of the Bi-Metric/Press-Fit Universal was higher than that for the reference group (88% (CI: 84–92) vs. 78% (CI: 74–82)). For patients aged 65–74 years also, the survival rate at 15 years of the Bi-Metric/Press-Fit Universal (95% (CI: 93–98)) was higher than that for the reference group (87% (CI: 86–89%)).

Survival of total hip replacements (cup + stem combinations) – all revisions

When all patients aged 55 years or more were analyzed as a single group, the survival rate at 15 years of the cementless designs was lower than that for the reference group. The Cox regression analysis revealed that during the first 7 years postoperatively, the ABG I/ABG II had a significantly reduced risk of revision compared to the cemented reference group (Table 7). Furthermore, the ABG II/ABG II combination was the only design to show an increased risk of revision during the first 7 years after the primary operation (Table 7). Beyond 7 years of follow-up, however, several cementless designs (the Anatomic Mesh/HG-II, the PCA Standard/PCA Pegged, and the ABG I/ABG I) showed higher risk of revision than the cemented reference group (Table 7, Figure 2B), and none of the cementless designs had a lower risk of revision than the reference group beyond 7 years. Beyond 7 years, the number of ABG I/ABG II THRs was low (Table 7).

During the first 7 years postoperatively in the patients aged 55–64 years, the risk ratio for revision of cementless THRs for any reason was not significantly different from that of the cemented reference group, except that the ABG I/ABG II had a reduced risk of revision compared to that of the reference group (RR = 0.45, CI: 0.28–0.72). Beyond 7 years of follow-up, the risk ratio for revision due of cementless THRs for any reason was not significantly different from that of the cemented reference group, except that the PCA Std/Pegged (RR = 2.0, CI:...
with poor results would be unlikely to have a major effect on the results in a study with such a high number of implants. Moreover, it is the purpose of registry studies to evaluate population-based results, including hospitals of variable standards. Another possible limitation of registry-based studies is their single definition of failure, i.e. a revision operation. There may be patients with osteolysis or loosened implants who are too ill to undergo revision surgery or who simply prefer not to do so. Furthermore, the adjustments in the Cox model in our study were performed only for 2 confounders: age and sex. Many other potential confounders, such as antibiotic prophylaxis or hospital operative volume, may be associated with the relationship between implant brand and revision rate.

The implant designs varied over the long study period (Table 1). Some of the 3 cemented designs we used as the reference group were implanted over the whole study period, starting in 1980. Any recent developments in cementing techniques that were adopted may have resulted in higher long-term survival rates for those prostheses that were implanted later in the study period (Herberts and Malchau 2000, Malchau et al. 2002). However, the cemented implants we chose were the best performing designs in the Finnish Register regardless of the time period they were implanted (Mäkelä et al. 2008b).

| A         | B       | C       | D       | E       | F       | G       | H       | I       | J       | K       | L       |
|-----------|---------|---------|---------|---------|---------|---------|---------|---------|---------|---------|---------|---------|
| Anatomic Mesh/SG II | 604 | 11.1 | 532 | 97 | (96–98) | 445 | 94 | (92–96) | 92 | 85 | (80–89) | 0.68 | (0.51–0.90) | 0.006 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         |         |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.75 | (0.53–1.06) | 0.1  |
| PCA Std/PCA Pegged | 508 | 11.6 | 433 | 92 | (90–95) | 354 | 83 | (80–87) | 148 | 71 | (66–76) | 1.48 | (1.19–1.83) | < 0.001 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 1.37 | (0.96–1.96) | 0.09 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 1.46 | (1.11–1.92) | 0.006 |
| Bi-Metric/PF | 2,687 | 8.8 | 2,035 | 98 | (97–98) | 1,192 | 96 | (96–97) | 145 | 90 | (87–93) | 0.37 | (0.29–0.46) | < 0.001 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.39 | (0.29–0.54) | < 0.001 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.34 | (0.25–0.47) | < 0.001 |
| Bi-Metric/Mallory | 637 | 8.8 | 517 | 99 | (98–100) | 275 | 96 | (94–98) | 10 | – | – | 0.36 | (0.23–0.58) | < 0.001 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.27 | (0.13–0.55) | < 0.001 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.48 | (0.26–0.88) | 0.02 |
| Bi-Metric/Vision | 2,055 | 3.4 | 152 | 99 | (98–99) | 0 | – | – | 0 | – | – | 0.37 | (0.23–0.60) | < 0.001 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.37 | (0.23–0.62) | < 0.001 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 2.53 | (0.35–18.4) | 0.4  |
| ABG I/ABG I | 565 | 9.1 | 455 | 97 | (96–99) | 330 | 92 | (90–95) | 0 | – | – | 0.75 | (0.54–1.04) | 0.09 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.51 | (0.29–0.87) | 0.01 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 1.03 | (0.68–1.55) | 0.9  |
| ABG I/ABG II | 1,765 | 5.9 | 700 | 99 | (99–100) | 14 | – | – | 0 | – | – | 0.12 | (0.06–0.22) | < 0.001 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.12 | (0.06–0.24) | < 0.001 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.13 | (0.02–0.93) | 0.04 |
| ABG II/ABG II | 1,489 | 2.5 | 0 | – | – | 0 | – | – | 0 | – | – | 0.33 | (0.15–0.74) | 0.007 |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 0.34 | (0.15–0.76) | 0.009 |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | – | – | – |
| Cemented | 9,549 | 8.8 | 6,234 | 96 | (96–96) | 4,447 | 93 | (93–94) | 1,116 | 88 | (87–89) | 1.0 | (reference) | – |
| FU ≤ 7 years |         |         |         |         |         |         |         |         |         |         |         | 1.0 | (reference) | – |
| FU > 7 years |         |         |         |         |         |         |         |         |         |         |         | 1.0 | (reference) | – |

1.3–3.3) had an increased risk of revision compared to the reference group.

**Discussion**

We found that the survival rate for aseptic loosening of the best performing cementless stems in patients aged 55–74 years was higher than that of the cemented reference stems. Biological fixation in itself seems to be a reliable method in THA of elderly patients. However, the survival rate of the cemented reference implants for any reason was higher than that of cementless implants. Polyethylene wear and osteolysis remain a serious problem with all cementless cup designs with unplugged screw-holes and poor liners. A longer follow-up is required in order to determine whether cups with plugged screw-holes and modern liner options provide any solution to the wear-problem.

Registry-based studies have certain limitations. The coverage of the Finnish Arthroplasty Register before the period 1994–1995 was only 90% (Puolakka et al. 2001a). The missing 10% of implant data may have caused bias in our study. It is also possible that only a few centers performed most of the implantations of certain designs. However, a single center with poor results would be unlikely to have a major effect on the results in a study with such a high number of implants. Moreover, it is the purpose of registry studies to evaluate population-based results, including hospitals of variable standards. Another possible limitation of registry-based studies is their single definition of failure, i.e. a revision operation. There may be patients with osteolysis or loosened implants who are too ill to undergo revision surgery or who simply prefer not to do so. Furthermore, the adjustments in the Cox model in our study were performed only for 2 confounders: age and sex. Many other potential confounders, such as antibiotic prophylaxis or hospital operative volume, may be associated with the relationship between implant brand and revision rate.

The implant designs varied over the long study period (Table 1). Some of the 3 cemented designs we used as the reference group were implanted over the whole study period, starting in 1980. Any recent developments in cementing techniques that were adopted may have resulted in higher long-term survival rates for those prostheses that were implanted later in the study period (Herberts and Malchau 2000, Malchau et al. 2002). However, the cemented implants we chose were the best performing designs in the Finnish Register regardless of the time period they were implanted (Mäkelä et al. 2008b).
Table 7. Survival of cementless total hip replacements and the cemented reference group. Endpoint was defined as revision of the cup and/or the stem for any reason. 7-, 10-, and 15-year survival rates were obtained from the Kaplan-Meier analysis. For an explanation of abbreviations, see Table 4

| A | B | C | D | E | F | G | H | I | J | K | L |
|---|---|---|---|---|---|---|---|---|---|---|---|
| 55–64 | | | | | | | | | | | |
| Anatomic Mesh/HG-II | 385 | 11.2 | 343 | 94 (92–97) | 296 | 89 (86–92) | 57 | 70 (64–76) | 1.18 (0.91–1.54) | 0.2 |
| PCA Std/PCA Pegged | 347 | 12.2 | 303 | 91 (88–94) | 262 | 83 (79–89) | 119 | 66 (61–72) | 1.32 (1.03–1.69) | 0.03 |
| Bi-Metric/PFU | 1,863 | 9.1 | 1,488 | 93 (92–94) | 872 | 86 (85–88) | 102 | 66 (61–72) | 1.18 (0.97–1.44) | 0.09 |
| Bi-Metric/Mallory | 266 | 9.0 | 224 | 95 (92–97) | 119 | 83 (77–88) | 8 | 72 (61–82) | 1.27 (0.90–1.80) | 0.2 |
| ABG I/ABG I | 746 | 6.0 | 309 | 95 (93–97) | 6 | – | – | – | 0.90 (0.62–1.31) | 0.6 |
| ABG I/ABG II | 610 | 2.4 | 0 | – | 0 | – | 0 | – | 1.54 (0.93–2.53) | 0.0 |
| Cemented | 1,204 | 9.5 | 837 | 92 (91–94) | 210 | 76 (72–79) | 58 | 70 (64–76) | 1.0 (reference) | – |
| Subtotal | 6,781 | | | | | | | | | |
| 65–74 | | | | | | | | | | |
| Anatomic Mesh/HG-II | 186 | 11.3 | 165 | 94 (90–97) | 133 | 90 (86–95) | 34 | 77 (67–87) | 1.05 (0.70–1.56) | 0.8 |
| PCA Std/PCA Pegged | 133 | 11.0 | 112 | 91 (86–96) | 85 | 81 (74–88) | 30 | 60 (50–70) | 1.78 (1.23–2.58) | 0.002 |
| Bi-Metric/PFU | 740 | 8.5 | 525 | 94 (92–96) | 320 | 90 (87–93) | 45 | 85 (81–89) | 0.89 (0.68–1.16) | 0.4 |
| Bi-Metric/Mallory | 274 | 8.8 | 223 | 95 (92–98) | 119 | 91 (87–95) | 119 | 66 (61–72) | 1.27 (0.90–1.80) | 0.2 |
| ABG I/ABG I | 238 | 9.0 | 187 | 91 (87–95) | 142 | 86 (81–91) | 0 | – | – | – |
| ABG I/ABG II | 789 | 5.9 | 311 | 94 (92–96) | 8 | – | 0 | – | 0.48 (0.31–0.75) | 0.001 |
| ABG II/ABG II | 647 | 2.4 | 0 | – | 0 | – | 0 | – | 1.62 (1.05–2.51) | 0.03 |
| Cemented | 4,964 | 9.3 | 3,446 | 92 (91–94) | 722 | 76 (72–79) | 210 | 76 (72–79) | 1.0 (reference) | – |
| Subtotal 8,821 | | | | | | | | | |
| >75 | | | | | | | | | | |
| Anatomic Mesh/HG-II | 33 | 8.9 | 25 | 90 (80–100) | 17 | – | 2 | – | 1.69 (0.54–5.32) | 0.4 |
| PCA Std/PCA Pegged | 28 | 7.6 | 18 | 89 (83–95) | 8 | – | 1 | – | 2.44 (0.78–7.66) | 0.1 |
| Bi-Metric/PFU | 97 | 8.1 | 73 | 98 (95–100) | 39 | – | 1 | – | 1.05 (0.81–1.36) | 0.7 |
| Bi-Metric/Mallory | 125 | 2.8 | 6 | – | 0 | – | 0 | – | 2.09 (0.92–4.77) | 0.08 |
| ABG I/ABG I | 47 | 8.0 | 33 | 100 (100–100) | 21 | 100 (100–100) | 0 | – | – | – |
| ABG I/ABG II | 230 | 5.6 | 82 | 97 (94–99) | 1 | – | 0 | – | 0.70 (0.31–1.60) | 0.4 |
| ABG II/ABG II | 232 | 2.6 | 0 | – | 0 | – | 0 | – | 1.69 (0.85–3.35) | 0.1 |
| Cemented | 3,381 | 7.6 | 1,954 | 96 (95–97) | 1,198 | 95 (94–96) | 186 | 94 (92–95) | 1.0 (reference) | – |
| Subtotal 4,257 | | | | | | | | | | |
| All (≥ 55 years) | | | | | | | | | | |
| Anatomic Mesh/HG-II | 604 | 11.1 | 532 | 94 (92–96) | 446 | 89 (87–92) | 93 | 72 (67–78) | 1.19 (0.97–1.47) | 0.1 |
| PCA Std/PCA Pegged | 28 | 7.6 | 18 | 88 (83–95) | 8 | – | 1 | – | 2.44 (0.78–7.66) | 0.1 |
| Bi-Metric/PFU | 354 | 8.8 | 2,044 | 93 (92–94) | 1,205 | 87 (86–89) | 147 | 71 (67–75) | 1.10 (0.95–1.27) | 0.2 |
| Bi-Metric/Mallory | 274 | 8.8 | 223 | 95 (92–98) | 119 | 91 (87–95) | 119 | 66 (61–72) | 1.27 (0.90–1.80) | 0.2 |
| Bi-Metric/Vision | 125 | 2.8 | 6 | – | 0 | – | 0 | – | 2.09 (0.92–4.77) | 0.08 |
| ABG I/ABG I | 47 | 8.0 | 33 | 100 (100–100) | 21 | 100 (100–100) | 0 | – | – | – |
| ABG I/ABG II | 230 | 5.6 | 82 | 97 (94–99) | 1 | – | 0 | – | 0.70 (0.31–1.60) | 0.4 |
| ABG II/ABG II | 232 | 2.6 | 0 | – | 0 | – | 0 | – | 1.69 (0.85–3.35) | 0.1 |
| Cemented | 3,381 | 7.6 | 1,954 | 96 (95–97) | 1,198 | 95 (94–96) | 186 | 94 (92–95) | 1.0 (reference) | – |
| Subtotal 4,257 | | | | | | | | | | |

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The proportional hazards assumption of the Cox model (meaning that the relative difference between revision rates should be constant over time since the primary operation) was not reached in some analyses. Thus, adjusted risk ratios were also established within time intervals (0–7 years and > 7 years after the primary operation). Follow-up beyond 7 years revealed that the results of cementless cups, and therefore of cementless THRs, deteriorate with time.

The revision rates that we found for cementless implants were similar to previous findings (Malchau et al. 1997, Thanner et al. 1999, Xenos et al. 1999, Archibeck et al. 2001, Puolakkka et al. 2001b, Giannikas et al. 2002, Bojescul et al. 2003, Jacobsen et al. 2003, Duffy et al. 2004, Herrera et al. 2004, Marshall et al. 2004, Moskal et al. 2004, Oosterbos et al. 2004, Kim 2005, Eskelinen et al. 2006, Castoldi et al. 2007, Firestone et al. 2007, Surdam et al. 2007).

We found a higher long-term survival rate for the Bi-Metric stem than for the reference stems in patients aged 55–74 years. When revisions for aseptic loosening were analyzed, the Press-Fit Universal cup was found to have a long-term survival rate similar to those of the reference cups in patients aged 55–74 years. In Finland, Biomet cups were used with Hexloc liners until 1995, and with Ringloc liners after that. In an earlier study based on data from the Finnish Register, survivorship of the Press-Fit Universal cups with Hexloc liners was poor (Puolakkka et al. 1999). Reasons for increased wear of Hexloc liners were thin polyethylene, poor quality of the polyethylene, cylindrical design, and a poor locking mechanism (Puolakkka et al. 1999, 2001b). Furthermore, the screw-holes of Press-Fit Universal cups were unplugged. In the present study, the survival rate of the Bi-Metric/Press-Fit Universal at 15 years was lower than that of the cemented reference group when all revisions were taken into account. However, the adjusted risk of revision of the Bi-Metric/Press-Fit Universal for any reason was similar to that of the reference group. This finding is probably influenced by the positive effect of Ringloc liners (starting in 1995) on the results with the Bi-Metric/Press-Fit Universal. Unfortunately, it is not possible to analyze the survival rate of the Press-Fit Universal cups with Hexloc liners and with Ringloc liners separately in the Finnish Register data. Revision risk for any reason with the Bi-Metric/Vision was similar to that for the cemented reference group (Table 7, Figure 2B). However, survival rates at 10-years for the Vision cup with Ringloc-liners and plugged screw-holes are not yet available. The survival rate for aseptic loosening of the Anatomic Mesh/Harris-Galante II at 15 years was not significantly different from that of the cemented reference group. Nonetheless, the survival rate of the Anatomic Mesh/HG-II for any reason at 15 years was poor. Again, this finding can be attributed to wear-related factors. The Anatomic Mesh/Harris-Galante II is no longer being implanted in patients in Finland.

The 15-year survival rate for the PCA Standard stem in our study was lower than those for the best-performing stems. The PCA Standard/PCA Pegged prosthesis is no longer being implanted in patients in Finland.

The 10-year survival rate of the ABG I/ABG I for any reason was lower than that for the reference group. However, the survival rate of the ABG I stem at 10 years for aseptic loosening was higher than that for the reference group. For this reason, and because of poor liners in the ABG I cup design, in Finland the ABG I stem has been widely used along with the ABG II cup with plugged screw-holes and thicker Duration liners consisting of stabilized polyethylene (Stryker, Mahwah, NJ). In our study, the risk of revision of the ABG I/ABG II for any reason in patients aged 65–74 was lower than that for the reference group when all revisions were taken into account (Table 7, Figure 2B). However, the survival rates for the ABG I/ABG II at 10 years are not yet available. Survivorship of modular cementless cups may dramatically worsen after 7–10 years of follow-up due to excessive wear and osteolysis, as indicated by the beyond-7-years survival analysis in our study. Thus, it is too early to draw any definite conclusions about the long-term success of this hip implant.

The ABG II stem differs from the ABG I stem regarding its titanium alloy composition, its stem geometry, its macrotexture, its conus size, and the option with Zirkonia heads (ABG II Cement-Free Hip System). The risk of revision of the ABG II/ABG II for any reason was higher than that for the reference group. The mean follow-up time for the ABG II/ABG II was short: only 2.5 years (Table 1). The proportion of periprosthetic fractures for all revisions of the ABG II/ABG II was high: 37% (Table 3). This finding is in accordance with clinical experience in Finland. The ABG II stem appears to be vulnerable to perioperative periprosthetic femoral fractures, due to its anatomical and conical shape. There were only 3 aseptic loosenings of the ABG II stem during the study period (Table 3). The problem with an early aseptic loosening of a cementless stem is that there may not have been any osseointegration at all from the beginning, due to undersizing or some other technical failure. Thus, strictly speaking any associated loosening could not have happened either. A longer follow-up time is needed to determine whether either the ABG I/ABG II or the ABG II/ABG II provides a long-term solution to the wear problem. Only a few Zirkonia head or liner fractures have been reported in Finland (Table 3).

For patients aged 75 years and older, the survival rates were similar between cementless implants and the cemented reference group, except that the PCA Pegged cup had an increased risk of revision compared to the cemented reference group. This is in accordance with the results of a previous report from the Finnish Arthroplasty Register (Mäkelä et al. 2008a). However, there was little information for this subgroup.

In conclusion, cementless, proximal porous-coated stems are a good option for elderly patients. Polyethylene wear and osteolysis remain a problem for cementless designs with unplugged screw-holes and low-quality liners.
No competing interests declared.

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