Lab-on-a-foil devices with integrated retro-reflective structures for multiplexed DNA testing

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Abstract

With the Covid-19-based global pandemic that started in the beginning of 2020, the vital importance of accelerated, reliable and affordable virus testing systems has once again become clearer. Besides, we all learned very well that the disposable biochips, to be used in these in vitro diagnostic (IVD) testing systems, supposed to be produced in large amounts in a very short time to be widely available for the use of humanity to save more and more lives. That is why; roll-to-roll (R2R) polymer structuring manners offer such large quantities for the production of in vitro biochips. Our technology, based on R2R UV nanoimprint lithography (UV-NIL), has superior features. Via our pilot line, robust 7500 biochip components per 100 meter of a flexible, polymer foil coated with a UV curable photo-resin (i.e., parts with capillary fluidic channels or optical structures for IVDs) can be generated. This study shows an example of a prototype of a R2R UV-NIL generated chip: a foil, capillary flow-based IVD biochip for multiplexed DNA detection purposes (i.e., a Lab-on-a-Foil device). The biochip performance was further increased dramatically by integrating UV-NIL produced retro-reflective microstructures, which reflects the light back, to its design to enhance optical signal detection in a commercial IVD device, detecting DNA on a chemiluminescent-reaction basis.

Introduction

Our R2R large-scale polymer imprinting technology provides parallel production of micro- or nano-structures on flexible polymer foils in a high-throughput manner (e.g., 7500 IVD biochip parts either bottom or top, per 100 meter) [1–6]. The process, which is performed at room temperature and ambient pressure, is based on UV-NIL structuring of a positive photo-resin, which is afore coated onto a polymer foil in the beginning of the process line. Our R2R UV-NIL pilot line was shown in Fig. 1. The flexible, transparent polymer foils can be rapidly structured via our imprinting technology in multifarious designs (e.g., capillary-based fluidic channels or pumps, optical structures for IVD chips) with various length scales. Using the foils with typical thickness of ~100 µm, obtaining robust structures with an aspect ratio up to 5:1 (depth: width) [2] is possible.

Therefore, our technology offers remarkable advantages, such as low cost, easy handling and high-throughput manufacturing for polymer-based and disposable in vitro diagnostic biochip production. In order to prove the performance of foil-based IVD chips, a model pathogen testing system with chemiluminescence-based target DNA detection was utilized in this study. A prototype foil DNA chip [1] was batch produced and integration of UV-NIL pyramidal retro-reflective (so-called RR) microstructures was done to investigate the performance of out-coupled light-enhancements in the presence of RR structures.
Experimental details

Production of the foil-chips

A prototype of our foil-based chip for R2R UV-NIL structuring, which was recently demonstrated in our previous study [1], was produced via a batch imprinting technique. The master structures (i.e., fluidic channels or RR microstructures) were written on a silicon wafer (Si-Mat, Germany) via photolithography. Then the structures were transferred onto a polydimethylsiloxane (PDMS) mold via soft-lithography, allowing 2.5-D topologies in a single-step production. To produce the PDMS mold, PDMS® Sylgard 184 Silicone Elastomer kit (a PDMS monomer and a curing agent, Sigma-Aldrich, Germany) was utilized. For this purpose, the polymer mould was custom-made by mixing the PDMS monomer curing agent with a ratio of 10:1 w/w, respectively. The mixture was casted over the master and cured on a hotplate for 24 h at 40 °C, sequentially. The PDMS mould was then detached from the wafer and cut into a final size for UV-NIL structuring purposes. The fluidic structures were transferred to a custom-developed photo-resin (NILcure JR21, Joanneum Research, Austria) coated on a polystyrene (PS) foil with thickness of 190 µm (4titude, Germany) by stamping. The curing of the photoresin with the imprinted structures was done using a UV-lamp (365 nm, Waldmann, Germany). To the upper chip parts, a glue was screen-printed prior to the chip bonding with the lower part [1]. The bottom chip part was a PS foil with probe DNA stripes printed using a capillary printer (BioDot™ Inc., USA). The DNA printing buffer contained Brilliant Blue G (Sigma-Aldrich, Germany) solution and GENSPEED printing buffer with probe ss-DNA concentration of 2 µM for each. The chip lamination was performed by combining the two parts using an office laminator. The UV-NIL structured RR microstructures were integrated at the upper part of the foil chip after bonding. A retro-reflective band (Reflexite® Visibly Better™) was used as master for the RR structures and was transferred to a PDMS mold. This mold was transferred to the top side of the chips by UV imprinting using the custom-developed photoresin NILcure JR21. Another custom-developed photoresin (mr-NIL500SF, micro resist technology, Germany) was utilized as an adhesion promoter. The structures were placed such that they serve as back-reflectors of the incident light generated via a chemiluminescent reaction in the chip. Therefore, a larger portion of the chemiluminescent light was guided towards the photodiodes increasing the signal collection efficiency.

The measurement protocol

The pipetting protocol for the foil-chips, is provided in Table 1. The chip performance testing was performed using a commercial IVD device: GENSPEED® R1, which provides rapid testing of hospital-acquired, methicillin-resistant Staphylococcus aureus (MRSA). The measurements were conducted at room temperature using GENSPEED® MRSA hybridization solution which gives positive signals for mecA, SA, PC and HC genes and negative signals for SE, NC and mecC genes. The concentration of all target ss-DNAs was 1 pmol/µl for each (except for HC targets) in the GENSPEED® hybridization solution. All full complementary DNA strands are 25 base-pair long except for HC, which is 105 base-pair long. The detection is based on DNA hybridization between surface bound ss-DNAs and biotinylated target ss-DNAs in the hybridization solution. The biotin is recognized by a streptavidin-horse radish peroxidase conjugate (SA-HRP) (i.e., commercial GENSPEED®

### Table 1 Experimental protocol of the foil-chips tested in GENSPEED® R1 device (GENSPEED Biotech, Austria).

| Reagent introduction steps | Injection time (s) | Volume (μl) | Total volume |
|---------------------------|-------------------|-------------|--------------|
| I. Hybridization solution | 0                 | 10          | 20           |
|                           | 60                | 10          |              |
| II. Enzyme solution       | 180               | 10          | 30           |
|                           | 210               | 10          |              |
|                           | 240               | 10          |              |
| III. Wash solution        | 300               | 10          | 40           |
|                           | 330               | 10          |              |
|                           | 360               | 10          |              |
|                           | 390               | 10          |              |
| IV. Chemiluminescent solution | 420            | 10          | 20           |
|                           | 450               | 10          |              |
enzyme solution). The excess of unbound molecules were removed at the washing step.

The solutions were and the testing procedure was described in detail, in our previous study [1]. The chemiluminescent light is then generated over the DNA-DNA- and biotin-SA-HRP-conjugation via chemiluminescent solution. All solutions are introduced manually into the chip inlet. The readings were done via the GENSPEED® R1 software. The generated light is detected by a photodiode array composed of 32 photodiodes (i.e., pixels), each with a size of 0.89 mm × 4.39 mm. The pixel distance is 0.1 mm in the photodiode array.

Data analysis

Using a custom-developed MATLAB® (MathWorks, USA) tool, the background subtracted net signal (a.u.) was calculated for each corresponding pixel location for printed ss-DNA stripes (the blue lines shown in Fig. 2-(4)) on the foil-chip. The integrated net signal (a.u.) was calculated by considering neighboring pixel (right and left) signals of each main pixel. Each data were provided as a mean value ± its standard deviation.

Discussion

The geometry of the UV-NIL produced retro-reflective structures at the upper side of the top biochip part (shown in Fig. 2-(1) and (2), the red zone on the chip) is shown in Fig. 3. The retro-reflective microstructures had a triangle edge and a height of 166 µm and 100 µm, respectively. In order to test the foil-chip performance, two types of chips were used (i.e., foil-chips with and without retro-reflective microstructures). The GENSPEED® R1 readings were analyzed via the MATLAB® tool and the result is provided in Fig. 4. As can be seen in Fig. 4, the modified foil-chips with the RR structures showed higher positive signals (a.u.) as compared to the unmodified foil-chips. The mecA net signal (a.u.), shown as yellow columns in Fig. 4, was dramatically enhanced by a factor of 2.7 in the presence of the RR structures. Likewise, signal enhancements were observed on also SA, PC and HC pixels (Fig. 4, purple, gray and pink columns, respectively). SA, PC an HC signals (a.u.) were enhanced in average 1.7-, 1.8- and 2.0-folds, respectively, as compared to plain foil chips, in the presence of RR micro-structures. All chip showed low net signals (a.u.) for the negative controls (i.e., SE, NC and mecC pixels), which were below the detection limit (500 a.u. as net signal), as expected.

Fig. 2 The illustration of our UV-NIL produced polymer foil-based DNA chip. The chip is composed of two polymer components. a The upper side of the top chip part. (1) The area of UV-NIL structured retro-reflective micro-structures. (2) The lower side of the top chip part, structured with capillary-based fluidic channels composed of (a) retarding (5 mm length, 200 µm width, 70 µm height), (b) reaction (37 mm length, 2.7 mm width, 70 µm height) and (c) waste channels (total chip height 100 µm). (3) The bottom chip part, at which seven different single-stranded DNAs (i.e., the probes) were printed for a multiplexed DNA detection (shown as blue stripes). (4) The inlet and the small ventilation holes shown both on (1) and (3) were laser drilled. The top chip part was screen-printed using a glue prior to lamination. b The illustration of pyramidal, retro-reflective micro-structures in (a)-(2)

Fig. 3 A scanning electron microscopy (SEM) image of the UV-NIL produced retro-reflective structures
Conclusions

This study shows for the first time retro-reflective microstructure integration into our R2R UV-NIL prototype, foil-based fluidic chip for multiplexed DNA detection purposes [1]. The experimental results revealed that the RR micro-structures on top of the fluidic biochips, significantly enhanced the optical signal collection efficiency and thus the signal at the detectors. Thereby, our results showed the applicability of our foil-based DNA chips, which give distinguishable signals for multiplexed detections, clearly using the commercial GENESPEED® R1 IVD product.

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Data availability  Due to confidentiality agreements, supporting data can only be made available to bona fide researchers subject to a non-disclosure agreement. Details of the data and how to request access are available from the corresponding author of this article.

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