Limited bioavailability of green tea polyphenols hampered their delivery to tumor and hence therapeutic effectiveness. This study investigated the antitumor activity of polyphenon-E (PE) encapsulated into chitosan nanoparticles (CSNPs) in Ehrlich solid tumor in mice. CSNPs-PE, with a particle size of 53–69 nm showed 83% entrapment efficiency and a sustained release of PE in pH = 7.4 at 37 °C. The data demonstrated a higher percentage of released drug in case of less crosslinked formulations. Ehrlich ascites carcinoma (EAC) cells (2.5 × 10⁶/0.2 ml/mouse) were injected subcutaneously in the back of mice. Oral administration of CSNPs-PE for 30 days produced a significant decrease in tumor volume (53%) and weight (60%) compared with free PE and voids CSNPs (72%). Compared with free PE and control, cell cycle revealed G0/G1 arrest associated with decrease in proliferating cell nuclear antigen (PCNA). In tumor tissue of CSNPs-PE treated mice, compared with free PE, there were: 1) induction of Bax and p53, 2) activation of caspases-3, -8 and -9, and CD95, 3) decrease in Bcl-2 expression of 4) inhibition of VEGF and CD31 expressions in tumor tissue. In conclusion, encapsulation of PE into CSNPs provided a good platform for cancer chemotherapy and raised existing application of different polyphenols for nanochemotherapy/prevention.

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while its effect on Ehrlich cell carcinoma was not fully studied. Therefore, the current study investigated the antitumor efficiency of oral treatment with polyphenon-E encapsulated into CSNPs on solid Ehrlich tumor model in mice.

Materials and methods

Chemicals

The polyphenon-E (PE), chitosan, (CS) of medium MW, % N-deacetylation about 81%, as determined by elemental analysis, and sodium tripolyphosphate bentapasic (STPP) were purchased from Sigma Aldrich (St. Louis, MO). Glacial acetic acid, phosphate-buffered saline (PBS), and all other reagents were of analytical grade. Anti PCNA, VEGF, CD31, P53, CD95, Bcl-2, BAX, and caspases 3, 8 and 9 antibodies were obtained from Thermo Scientific. Mouse monoclonal antibody (Cat No MS-106-P0, USA), (Thermo scientific, Rabbit polyclonal antibody, Cat No RB-9031-P0, USA), (Thermo scientific, Rabbit polyclonal antibody, Cat No RB-10333-P0, USA), (rabbit IgG antibody Lot No: GR 110207–1 abcam USA), (Mouse IgG1 primary antibody Lot No: 5120612021 Milteny Biotec), (mouse IgG1 antibody CodeNo: F7053 DAKO/S Denmark), (monoclonal IgG antibody Lot No: GR142124-1 abcam USA), (Cat No 51-68654X Lot:16374 Rabbit IgG BD Biosciences USA), (Rabbit monoclonal primary antibody ab 32125 Lot No: YH080907D abcam USA and goat pAb to Rabbit IgG as a secondary antibody (Lot No: 15232–1 abcam USA), and (Rabbit monoclonal IgG antibody Lot No: GR63053-2 abcam USA), respectively.

Preparation of polyphenon-E loaded CSNPs

Chitosan nanoparticles (CSNPs) were prepared using ionotropic gelation technique [20] with a slight modification. Briefly, an aqueous CS solution (0.1% w/v) was obtained by dissolving CS in 0.1% w/v acetic acid. Then, 0.1% STPP aqueous solution was added drop wise to CS solutions under mild magnetic stirring for 20 min. Opalescent suspensions were formed spontaneously at room temperature which were further examined as the hydrogel NPs. The PE-60 loaded CSNPs were prepared using the same procedure but with dissolving a 250 mg/kg body weight of the PE-60 in the CS solution.

Morphology and particle size measurements

The morphology and particles size measurements of the developed hydrogel NPs were performed by transmission electron microscopy (TEM, JEOL, JEM-1230, Japan Ltd.) at accelerating voltage of 200 kV. Samples were prepared for imaging by drying the NPs on a copper grid that is coated with a thin layer of carbon. The size of the plain and PE-60-loaded CSNPs was also determined by dynamic light scattering (DLS) (Malvern nanosizer, Malvern Instruments Ltd., Worcestershire, UK).

Swelling behavior of NPs

The swelling behavior of the freeze-dried plain CSNPs was studied by incubating certain amount of the dry particles (10–15 mg) in an Eppendorf tube containing 1.5 ml of PBS (pH 7.4) with shaking at 120 rpm at 37 °C. At certain intervals, swollen samples were separated from the PBS solution and weighted to calculate their swelling percentages using the following relationship:

\[
S(\%) = \frac{W_t - W_0}{W_0} \times 100
\]

where \(W_0\) is the initial weight and \(W_t\) is the weight of the swollen particles at time t. The swelling data represents the average ± SD from three independent swelling experiments.

Drug entrapment efficiency

The entrapment efficiency (EE%) of PE-60 was determined via separation of the PE-60-loaded CSNPs from a certain volume of their aqueous suspension by ultra-centrifugation at 14,000g and 4 °C for 20 min (SORALL® Bioguge Stratos Ultracenrifuge) followed by determination of the unloaded amount of PE-60 remaining free in the supernatant using UV-Vis spectrophotometry (Evolution™ 300 UV-Vis spectrophotometer, Thermo Scientific, USA) at \(\lambda_{max}\) of 442 nm. The entrapment efficiency (EE%) of the PE-60 was then calculated according to the following relationship:

\[
EE\% = \left(\frac{m_i}{m_r}\right) \times 100
\]

where \(m_i\) and \(m_r\) are the amounts (mg) of the PE-60 initially loaded and remained in the NPs, respectively.

In vitro release study

The in vitro cumulative release study of PE-60 from the developed CSNPs was carried out in PBS (pH 7.4). Briefly, the PE60-loaded CSNPs were separated from the prepared aqueous suspension by ultra-centrifugation at 14,000g and 4 °C for 20 min (SORALL® Bioguge Stratos Ultracenrifuge) followed by lyophilization of the precipitate. Then, the release study was carried out through incubating pre-weighed samples of the dry powder (10–15 mg) while shaking at 120 rpm in 2 ml of buffer solutions, PBS (pH 7.4) at 37 °C. After incubation, 100 μl aliquots were removed from the buffer solution to be analyzed by UV-Vis spectrophotometry (Evolution™ 300 UV-Vis spectrophotometer, Thermo Scientific, USA) at \(\lambda_{max}\) of 442 nm. The withdrawn sample was replaced with equal volume of fresh buffer solution to keep the volume of release fluid constant. The collected data represents the mean ± SD from three independent release experiments.

Animal grouping

The current study was conducted on female albino mice weighing 25–30 gm purchased from Cairo Oncology center. They were housed in standard sized cages under standard laboratory conditions (26 °C, 12 h light/dark cycle). Ehrlich Ascites carcinoma cells were obtained from Cairo oncology center. Treatment of animals was carried out following the guide for care and use of experimental animals according to Institutional Animal Ethics Committee (IAEC) of Mansoura University. All animal were injected with 2 × 10⁶ Ehrlich ascites carcinoma cells (EAC) (0.2 ml/mice) subcutaneously on the back of each mouse. Day of injection was assigned as day 0. On day 5 the animals were randomized and divided into 4 groups each containing 10 animals: Control group (C), which mice were transplanted with EAC cells. The second group was orally administrated with 0.1 ml chitosan nanoparticles (Cs) on day 5 after transplantation 3 times a week for 30 days. The third group (CSNPs–PE) was administrated with CSNPs–PE on day 5 of EAC cells injection 3 times a week for 30 days with total volume 0.1 ml orally using stomach tube. The forth group (PE) was orally administrated with 0.1 ml free polyphenon-E (PE) on day 5 after transplantation 3 times a week for 30 days. In all cases the concentration of the PE is 250 mg/kg body weight.

After completion of the experimental period of 30 days, overnight fasted animals were sacrificed and tumors were excised.

Tumor weight and volume

A noninvasive standard method for determination of tumor volume was used [21]. Tumor volume was measured using external
caliper starting from 10th day after transplantation of tumor cells and subsequently recorded every week along the experimental period of 30 days. Tumor volume was estimated by the modified ellipsoidal formula.

**Tumor volume** = \(\frac{1}{2} (\text{length} \times \text{width}^2)\)

After completion of experimental period of 30 days, overnight fasted animals were sacrificed and tumors were excised and weighted.

Each tumor was divided into two portions for immunocytochemical, biochemical and molecular investigations.

**Molecular determination**

Solid tumor preparation for Flow Cytometry was performed by mechanical dissociation technique [22].

**Cell cycle analysis**

The obtained tumor cells were permeabilized, fixed then nuclear DNA was labeled with propidium iodide (PI) using Cycle TEST PLUS DNA reagent kit [23]. The distribution of nuclear DNA of cell cycle phase was determined on FACS, fluorescence detector using Cell Quest software (Becton Dickinson). A total of 10,000 events was acquired and analysis of flow cytometric data was performed using Mod Fit software. A histogram of DNA content versus counts has been displayed.

**Apoptosis analysis**

Annexin-V FITC/PI, ApoAlert kit from Clontech (Palo Alto, CA) was used to distinguish between apoptosis and necrosis according to the instructions described by the manufacturer. Before staining, cells were fixed using 2% paraformaldehyde and permeabilized with Saponin, (0.5% v/v in PBS, pH 7.4). The cells were washed and suspended in PBS (pH 7.4) with 0.2% BSA, divided into aliquots for flow cytometric analyses. The flow cytometry analyses were performed on an FACS CaliburTM cytometer (BD Biosciences, San Jose, CA) using CellQuest Pro software (Becton Dickinson) for data acquisition and analysis [24]. A total of 10,000 events were acquired and the cells were properly gated for analysis.

**Determination of proliferation marker, and pro- and anti-apoptotic proteins**

For determination of the expression of p53, Bax, Bcl-2, CD95 and caspases 3 and 9, tumor cells were permeabilized and fixed as described earlier. Cells (1X10^6) from each group were incubated for 30 min with anti-Bcl-2 antibody, anti-Bax antibody for flow cytometry analysis of Bcl-2 and Bax, respectively. A mouse anti-P53 FITC, was used for p53 analysis by flow cytometry. In case of

![Fig. 1. Schematic illustration of the prepared polyphenon-E-loaded chitosan nanoparticles.](image-url)
caspases 3, 8 and 9 FITC rabbit anti-active caspase 3, anti-caspase 8 antibody or rabbit monoclonal anti-caspase 9 (E23) antibody were used respectively. Cells were washed thoroughly with PBA/BSA, centrifuged at 400g for 5 min, re-suspended in 0.5% paraformaldehyde in PBS/BSA and analyzed on a Flow cytometer equipped with 488 nm Argon laser light source and a 515 nm band pass filter for FITC-fluorescence. A total of 10,000 events were acquired and the cells were properly gated for analysis.

**Immunohistopathological assessment**

Tumor tissues were fixed in 10% neutral-buffered formalin, and embedded in paraffin and 5μm sections were prepared for staining. The proliferating cell nuclear antigen (PCNA), platelet endothelial cell adhesion molecule-1 (PCAM/CD31) and vascular endothelial growth factor (VEGF) were obtained from Thermo-Fisher Scientific, USA with the following specifications; (PCNA, Mouse monoclonal antibody, MS-106-P0, USA), (CD31, rabbit polyclonal antibody, RB-10333-R7) and (VEGF, rabbit polyclonal antibody, RB-9031-R7). Immunohistochemical studies were performed by incubating tumor sections with suitable dilutions 1:50–1:400 primary antibodies. Negative control sections were prepared without primary antibody. All tissue sections were inspected using light microscopy to obtain images using Olympus (IX51) microscope [25].

The PCNA and VEGF were assessed and scored independently by two investigators using light microscopy. The numbers of positive cancer cell nuclei were scored in 400 cancer cells and the ratios of stained to total cells expressed as percentage were defined as PCNA or VEGF indices [23]. Scoring of CD31 expression was performed on computer assisted digital image analysis (Digital morphometric study). Tissue sections were photographed using Olympus digital camera fitted on Olympus microscope. The images of tissue sections were analyzed using Video-Test Morphology software (Russia) adapted for percent area measurement and object counting.

**Results**

**Preparation and characterization CSNPs and CSNPs-PE**

Chitosan nanoparticles (CSNPs) were prepared using ionotropic gelation technique as illustrated in Fig. 1. The average particle size of the void CSNPs (A1 and A2) and the PE-loaded CSNPs (A1-D and A2-D) obtained at different STPP concentrations was determined...
using dynamic light scattering and shown in Table 1. The data show that increasing the STPP content tends to reduce the size of the resulting NPs. For instance, the size of the void CSNPs A1 has reduced from 21.4 ± 7.6 nm to 16.7 ± 9.2 nm upon doubling the volume of the crosslinking agent, STPP. The same result was also noted in the case of PE-loaded NPs (A1-D and A2-D). The incorporation of the bioactive constituent, PE has increased the particle size as compared to the corresponding plain CSNPs (Table 1). CSNPs-PE, with a particle size between 53 and 69 nm was determined by dynamic light scattering and transmission electron microscopy. These particle size results were also confirmed from the obtained TEM micrographs shown in Fig. 2 (A and B). The TEM micrographs also demonstrated an almost spherical morphology of the prepared NPs. The entrapment efficiency (EE%) of PE in the developed CSNPs was determined and found to be in the range between 83.0 ± 2.1 to 86.3 ± 1.6% depending on the content of the crosslinking agent, STPP (Table 1).

Swelling ability of the prepared NPs is one of the key characteristics that determine their appropriateness for various biomedical applications. The swelling behavior of the void CSNPs obtained at different STPP concentrations (A1 and A2) was studied as shown in Fig. 2C. The data reveals that increasing the STPP content in the NPs tends to reduce the swelling values attained at equilibrium.

The cumulative release pattern of the loaded PE from the CSNPs of different crosslinking extents in PBS (pH 7.4) at 37 °C is illustrated in Fig. 2D. As shown in the figure, the percent of PE released increased gradually with time until attaining almost constant value after about 3–4 h. The data also demonstrates a relatively higher percentage of the drug released in the case of the less crosslinked formulation (A1) as compared to the more crosslinked nanoparticles (A2).

### Antitumor response

The antitumor effect of chitosan nanoparticle encapsulating polyphenon-E (CSNPs-PE) against EAC tumor implanted in mice was demonstrated by assessing tumor weights (Fig. 3A), and tumor volume (Fig. 3B) 30 days after EAC cell inoculation. The EAC-bearing mice demonstrated a significant increase in tumor weight and volume. Compared to the tumor-bearing mice, void CS-NPs, free PE and CSNPs-PE treatment resulted in significant reductions in tumor weights by 53%, 60% and 72% respectively. Similar trend was demonstrated in the tumor volume which significantly reduced along the experimental period when CSNPs-PE has been given orally. In all cases CSNPs-PE produced a pronounced inhibitory effect on tumor weight and volume than Free PE.

To investigate if the reduction in tumor growth induced by CSNPs-PE administration is due to inhibition of tumor cell proliferation, we analyzed the cell cycle using flow cytometer. The percentage of cells in S-phase was decreased (P < 0.05) from approximately 25.09 ± 1.76% in tumor bearing control mice to 4.13% ± 0.21% and 9.90% ± 1.4% treated with CSNPs-PE and PE respectively (Fig. 4). The cell cycle analysis also revealed cycle arrest at G0/G1 in tumors obtained from mice treated with CSNPs-PE and PE respectively.

The proliferating activity of the tumor was studied by evaluating the related cell cycle antigen expression, the proliferating cell nuclear antigen (PCNA) using immunohistochemical approach on formalin-fixed paraffin embedded tumor (Fig. 5). Encapsulation of PE in CS-NPs produced a significantly higher inhibition in the PCNA expression by 56% than control tumor. In addition, the void CSNPs and free PE treated group showed remarkable reduction in the PCNA expression by 33% and 40% respectively compared to the tumor-bearing control group (Fig. 5A). The flow cytometer analysis of p53 levels in tumor tissue of Ehrlich carcinoma bearing mice under different conditions is shown in Fig. 5B. Associated with increased apoptosis, p53 significantly elevated in tumor tissue from mice treated with CSNPs-PE two fold compared with void CSNPs and free PE-treated EAC-bearing mice (Fig. 5B).

Fig. 6 shows the immunohistochemical detection of VEGF and CD31 in different tumor bearing mice. After 30 days, the VEGF in CSNPs-PE-treated group diminished significantly by 34% compared with the tumor-bearing control group. Oral administration of void CSNPs or free PE reduced the VEGF by 15% and 27% respectively when compared with the control group (Fig. 6A). Meanwhile, the

### Table 1

| Formulation | CS (% w/v) | STPP, (0.1% w/v) (ml) | Average particle size (nm) ± SD | EE% ± SD |
|-------------|------------|-----------------------|---------------------------------|----------|
| A1          | 0.1        | 10                    | 21.4 ± 7.6                      | –        |
| A2          | 0.1        | 20                    | 16.7 ± 9.2                      | –        |
| A1-D        | 0.1        | 10                    | 69.8 ± 7.7                      | 83.0 ± 2.1|
| A2-D        | 0.1        | 20                    | 53.1 ± 14.6                     | 86.3 ± 1.6|

*Fig. 3. Effect of polyphenon-E (PE) encapsulated into chitosan nanoparticles (CSNPs-PE) on (A) body weight changes and (B) tumor volume. EAC cells (2x10^6 cells/mouse) were injected subcutaneously to induce solid tumor in Swiss albino mice. CSNPs-PE was orally administered daily for 30 days. Values are mean ± SEM of three determinations. *P < .05 vs control group and **P < .05 vs PE-treated group.*
immunohistochemical expression of the endothelial markers, CD31 in EAC as possible evidence of vasculogenic mimicry was investigated (Fig. 6B). Immunostaining with antibodies against CD31 revealed that control bearing tumor mice showed significantly higher immunostained tumoral cells than other treated groups. The CSNPs-PE-treated groups showed markedly lower immunostained tumoral cells than CSNPs and PE-treated animals (Fig. 6B). These data suggest that PE inhibited the neoangiogenesis in tumor tissues and the CSNPs-PE is more efficient than PE alone.

Annexin/PI-labeled fluorescent technique was used to determine if the growth-inhibitory effects of CSNPs-PE correlated with enhanced induction of apoptosis. The data showed increased numbers of apoptotic cells and significantly (P > .001) lower numbers of live cells obtained from mice treated with CSNPs-PE compared with the control tumor bearing mice (Table 2 and Fig. 7). CSNPs-PE also produced a significant increase in the necrotic cell compared with the control tumor mice. The staining with annexin-V of tumor cell obtained from void CSNPs and free PE-treated mice showed increased apoptosis by 9% and 22% compared to control tumor. The data also show the apoptotic cells in case of CSNPs-PE-treated mice is significantly (P > .001) higher than free PE-treated rats. This effect is reflected on the percentage of live cells that is significantly lower in CSNPs-PE than free PE and CS treated rats. These findings indicate that the effect is more prominent with CSNPs-PE than free PE indicating the advantage of the catechin encapsulation in CS nanoparticles.

The proteins expression involved in apoptosis were evaluated and displayed in Fig. 8(A) and a representation of the flow cytometer charts is indicated in Fig. 8(B). The expression of Bax was increased by CSNPs-PE oral treatment. Concurrently, the expression of Bcl-2 was decreased by CSNPs-PE (Fig. 8). The data also showed the advantage of encapsulated PE compared with native PE and CSNPs. There was a significant increase in activation of the caspases 3, 8 and 9 respectively in the animals treated with CSNPs-PE as compared to free PE and void CSNPs (Fig. 8). The changes indicated that the encapsulated form of PE is more effective than the native PE. A significant increase in the expression of CD95 demonstrated in the EAC cell obtained from tumor-bearing mice treated with CSNPs-PE compared with void CSNPs and natural PE (Fig. 8).

Discussion

Tea catechins have remarkable antitumor impact, however they demonstrated a limited pharmacological application in clinical settings due to their poor in vivo stability, limited bioavailability, degradation in the gastrointestinal canal and inadequate intestinal absorption [7]. CS nanoformulations for drug delivery showed to enhance bioavailability and increased the absorption of tea polyphenols [26,27]. CSNPs were prepared by reaction of amino group of CS with phosphate group of STPP in aqueous medium. The synthesized CSNPs provided a formulation for green tea catechins to be embedded in the polymeric network [11], and therefore green tea catechins can be protected from degradation in the harsh milieu of the stomach and the gastrointestinal tract [28]. This was supported by a steady sustained release of the PE and in agreement with the swelling pattern of the particles and drug release (Fig. 2). The concentrations of CS and STPP are important to define the size
Fig. 5. Effect of polyphenon-E (PE) encapsulated into chitosan nanoparticles (CSNPs-PE) on expression of PCNA (A) and p53 (B) in tumor tissues of mice. Tumor sections were stained using specific antibodies. Counterstaining was performed with hematoxylin. Photomicrographs (magnification, ×20) show representative pictures from two independent samples (A). P53 was estimated using flow cytometer (B). *P < .05 vs control group and **P < .05 vs PE-treated group. CSNPs-PE downregulated PCNA and upregulated p53 in tumor tissue.

Fig. 6. Effect of polyphenon-E (PE) encapsulated into chitosan nanoparticles (CSNPs-PE) on expression of angiogenic indicators VEGF and CD31 in tumor tissues of mice. Tumor sections were stained using specific antibodies. Counterstaining was performed with hematoxylin. Photomicrographs (magnification, ×20) show representative pictures from two independent samples. *P < .05 vs control group and **P < .05 vs PE-treated group. CSNPs-PE downregulated expressions of VEGF and CD31 in tumor sections indicating inhibition of angiogenesis.
of NPs. After several trials, we used this particular preparation to synthesize spherical NPs with 53–69 nm and with 83% entrapment efficiency. Reports have shown that using NPs made from CS can improve biocompatibility and decrease possible toxicity [29]. This is consistent with reported work that CSNPs enhanced the plasma exposure of EGCG in mice through an enhancement in intestinal stability [7]. This lends credence to the newly developed CSNPs-PE that can enhance and extend the intestinal absorption of PE. In addition, CSNPs can adhere to the mucosa of the intestinal membrane and open up the tight junction between epithelial cells [30].

The main objective of the present nanoformulation CSNPs-PE was to enhance the antitumor effect of green tea catechin in Ehrlich tumor in vivo and to evaluate the effect of CSNPs-PE versus free PE on tumor growth and proliferation. The present data demonstrated that CSNPs-PE remarkably reduced the tumor growth in terms of tumor volume and weight compared with tumor implanted mice and mice who received free PE and void CS. The oncoprotein p53 that is essential for the inhibition of cell proliferation via impeding cell cycle progression and induction of apoptosis [31] was significantly increased in Ehrlich tumor after oral treatment with CSNPs-PE compared with free PE and void CS.

The cell cycle progression was analyzed to investigate if the reduction in tumor growth induced by CSNP-PE administration is due to inhibition of tumor cell proliferation. The percentage of cells in S-phase was significantly decreased in tumor obtained from CSNPs-PE than PE treated and control mice indicating the effectiveness of nanoformulation. The cell cycle analysis also revealed cycle arrest at G0/G1 in tumor obtained from mice treated with CSNPs-PE compared with other treated groups. These data also demonstrated that PE in nanoformulation is more effective than free PE. Furthermore, The CSNPs-PE group tumors, relative to control tumors, had significantly decreased PCNA expression that matched to the reduced cell population in S-phase results suggesting a decrease in the proliferation of tumor cells by CSNPs-PE. These data also support the reduced tumor growth observed in this study.

The prime pathway followed by cancer cells is to suppress apoptosis and p53 function; therefore appropriate anticancer treatments would stimulate apoptotic mechanisms and regain p53 activity to inhibit cancer proliferation. Apoptosis consists of

Table 2
Effect of polyphenon-E (PE) encapsulated into chitosan nanoparticles (CSNPs-PE) on EAC apoptosis and necrosis using flow cytometry. In a double label system, unfixed EACs from different animal groups of tumor-bearing mice were labeled with PI and Annexin V Fluos and then fixed and analyzed on a Flow cytometer.

|                | Control | CS    | CSNP-PE | PE     |
|----------------|---------|-------|---------|--------|
| A-viable cells | 75.15 ± 3.32 | 55.27 ± 3.9 | 27.70 ± 1.57 | 41.58 ± 1.26 |
| B-necrotic cells | 1.19 ± 0.07 | 1.44 ± 0.29 | 5.33 ± 0.79 | 1.83 ± 0.29 |
| C-early apoptotic cells | 10.06 ± 2.25 | 4.64 ± 1.52 | 13.16 ± 1.82 | 26.53 ± 3.60 |
| D-late apoptotic cells | 14.60 ± 2.21 | 38.65 ± 2.53 | 53.81 ± 2.60 | 31.38 ± 1.04 |

*P < .05 vs control group and **P < .05 vs PE-treated group.

Fig. 7. Flow cytometry data showing examples of the data generated by FACS. Dual parameter dot plot of FITC-fluorescence (x-axis) versus PI-fluorescence (y-axis) has been shown in logarithmic fluorescence intensity. The events shown in the lower left quadrant represent viable cells, and the upper left quadrant is indicative of necrotic cells that have taken up the PI. The percentage of early apoptotic cells that are Annexin V positive only is represented in the lower right quadrant, and events depicting late apoptotic cells that are Annexin V / PI positive are shown in the upper right quadrant. CSNPs-PE produced remarkable late apoptosis and necrosis. Values are mean ± SEM of three determinations. *P < .05 vs control group and **P < .05 vs PE-treated group.
Fig. 8. (A) Percent expression of Bcl-2, Bax, CD95, and caspases 3, 8, and 9 of EAC cells from EAC-bearing animals of all groups measured by flow cytometry using specific antibody. Values are mean ± SEM of three determinations. *P < .05 vs control group and **P < .05 vs PE-treated group. The CSNP-PE oral treatment for 30 days showed increased expressions of Bax, CD95, and caspases-3, 8, and 9 and downregulated Bcl-2 expression in tumor. (B) Flow cytometry data showing examples of the data generated by FACS.
mitochondrial and transmembrane death receptors pathways which comprise of the activation the effector caspases via the initiator caspases in cell death [32]. Consistent with increased expression of p53 in Ehrlich tumor of mice treated with CSNPs-PE, there was greater activation of CD96, caspases 3, 8 and 9 with up-regulation of Bax and down-regulation of Bcl-2 compared to free PE and void CSNPs. Changes in the Bax to Bcl-2 ratio resulted in the destabilization of the mitochondrial membrane and liberation of the proteolytic caspases and cleavage of PARP [33] that lead to cell death [3].

These results confirm previous study that PE increased lung cancer cell death by inhibition of Bcl-2 related apoptosis through reducing mitochondrial membrane potential and enhancing PARP cleavage [34]. Furthermore, PE induced growth inhibited in colon cancer cells [35]. The later authors demonstrated similar potencies of PE and EGCG and preferred PE for easier preparation and synergistic effect of mixed catechins. In a recent report, PE caused severe and prolonged endoplasmic reticulum stress in prostate cancer cells leading cell death through a caspase-independent pathway of necrosis [15].

It is well known that p53 functions to stimulate protective mechanisms against tumor growth by regulating the expression of both Bax and Bcl-2 [36,37]. It also acts as a tumor suppressor through its capacity to induce cell cycle arrest and apoptosis in response to a variety of chemotherapeutic drugs [38]. These results confirm other studies in which induction of apoptosis by tea polyphenols mediated in mouse skin tumors [39] and human fibrosarcoma HT-1080 cells through intrinsic cell death pathways in mouse skin tumors [39] and human fibrosarcoma HT-1080 cells [40]. Similarly, Epigallocatechin-3-gallate induces apoptosis in estrogen receptor-negative human breast carcinoma cells via modulation in protein expression of p53, Bax and caspase 3 activation [41]. Thus, CSNPs-PE played an important role to influence p53 to transduced signals into tumor-suppressive apoptotic and growth arresting responses. In addition, oral treatment with CSNPs-PE can induce apoptotic changes including activation of Bax, caspases 3, 8, and 9, and p53 and abrogated the activation of Bcl-2 in Ehrlich tumor (Fig. 9).

Angiogenesis is largely essential for tumor development and expansion of tumor mass because neovascularization permits rapid tumor growth by providing an exchange of nutrients, oxygen, and paracrine stimuli to the tumor [42]. Therefore, in this study, we used immunohistochemical staining for CD31 and VEGF, as markers of angiogenesis, to determine the effect of free PE and encapsulated nanoform on Ehrlich tumor angiogenesis in mice. CSNPs-PE-treated tumor had reduced angiogenesis than the free PE tumor as compared with control tumor. These results also suggest that a pronounced decrease in tumor angiogenesis is associated with a decrease in tumor size of Ehrlich tumor in the female mouse treated with CSNPs-PE compared to those in the control mice. There are several mechanisms described for the antiangiogenic effect of tea catechins. This includes a decrease tumor cell VEGF synthesis, a decrease in its binding to VEGF receptors [43], and inhibition of VEGF receptor phosphorylation [44,45]. Thus, CSNPs-PE exhibited anti-angiogenic effect by inhibiting VEGF and CD31 to prevent the communication between the tumor and its microenvironment and ultimately impede tumor growth and expansion (Fig. 9).

The major disadvantage associated with inability of many natural compounds in clinical setting is their limited bioavailability [2]. The present study overcome this limitation and demonstrated remarkable anticancer effect of PE encapsulated in CSNPs than free PE. In more recent study, EGCG encapsulated in CSNPs showed significant longer half-life than free EGCG indicating that nanoformulation increased stability and bioavailability leading to better clinical results [3]. The advantage of high surfaces area to volume ratio and ultra-small size of NPs suggests an increased in their conjugation with tumor cells which characterized by bigger size leading to more medical efficacy [46]. In addition, the biodegradability and biocompatibility of CS eliminates possibility of any systemic toxicity [1,47]. It is interesting that void CS showed antitumor effect nevertheless, it is less than encapsulated PE. Chitosan is
highly biodegradable and used as immunoadjuvant in cancer therapy [48] to enhance the photodynamic therapy of tumors [49]. This observation in agreement with previous study using CS encapsulated tea polyphenols on HepG2 cells [50] offering additional advantage to medical utility of CS.

In conclusion, encapsulation of PE in chitosan nanoparticles provide good platform for cancer chemotherapy and possess strong rational for further trials with different cancers and raise exiting application of different polyphenols for nano-chemotherapy/prevention.

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