Laminin-Modified Dental Pulp Extracellular Matrix for Dental Pulp Regeneration

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Native dental pulp extracellular matrix (DPEM) has proven to be an effective biomaterial for dental pulp regeneration. However, as a significant extracellular matrix glycoprotein, partial laminins were lost during the decellularization process, which were essential for odontoblast differentiation. Thereby, this study investigated the feasibility of LN supplementation to improve the surface of DPEM for odontoblast layer regeneration. The influences of laminin on cell adhesion and odontogenic differentiation were evaluated in vitro. Then, we fabricated laminin-modified DPEM based on the physical coating strategy and observed the location and persistency of laminin coating by immunofluorescent staining. Finally, laminin-modified DPEM combined with treated dentin matrix (TDM) was transplanted in orthotopic jaw bone of beagles (n = 3) to assess the effect of LNs on dental pulp tissue regeneration. The in vitro results showed that laminins could improve the adhesion of dental pulp stem cells (DPSCs) and promote DPSCs toward odontogenic differentiation. Continuous odontoblastic layer-like structure was observed in laminin-modified DPEM group, expressing the markers for odontoblastogenesis, dentine matrix protein-1 (DMP-1) and dentin sialophosphoprotein (DSPP). Overall, these studies demonstrate that the supplementation of laminins to DPEM contributes to the odontogenic differentiation of cells and to the formation of odontoblast layer in dental pulp regeneration.

Keywords: laminin, dental pulp, extracellular matrix, odontoblast, regeneration

INTRODUCTION

Dental pulp is a loose connective tissue containing vasculature and nerves as well as some specific cells, such as odontoblasts, to ensure the physiological properties of the dentine (Xuan et al., 2018). However, bacteria sometimes invades the pulp tissue to cause pulpitis, pulp necrosis, and subsequent apical periodontitis, which are commonly treated by removing the pulp and replacing it with inorganic materials via root canal treatment (RCT) (Eramo et al., 2018). This traditional treatment does not restore the biological function of the pulp.

Over the past 30 years, tissue-engineered approaches have been recognized as a promising future treatment model for achieving pulp healing and regeneration (Kawashima and Okiji, 2016). To date, there is compelling evidence that native extracellular matrix (ECM) material could retain its inherent structural, biochemical, and biomechanical cues of tissues or organs...
integrins, syndecans, and molecules and bind cells through cell surface receptors, including during organogenesis, laminins could interact with many ECM (Chen et al., 2015a). The α integrins and α- and β-dystroglycan, modulating cellular phenotypes and differentiation (Yap et al., 2019). During organogenesis, laminins could interact with many ECM molecules and bind cells through cell surface receptors, including integrins, syndecans, and α-dystroglycan, modulating cellular phenotypes and differentiation (Yap et al., 2019).

In the light of this consideration, the loss of laminins may affect the formation of the odontoblast layer and thus the effect of pulp regeneration. Therefore, we speculate that the supplementation of laminin in DPEM may contribute to regenerate a complete and continuous odontoblast layer. We have designed laminin-modified DPEM for dental pulp regeneration in the present study and have determined the feasibility for the repair of the odontoblast layer using laminin for a biofunctional scaffold coating.

**MATERIALS AND METHODS**

**Experimental Design**

The overview of the experimental design can be obtained in Figure 1. DPEM was fabricated from the dental pulp tissues of swine. Laminins from Engelbreth-Holm swarm murine sarcoma BM were used to coat the surface of DPEM. In order to observe dental pulp regeneration in vivo, the premolars were first extracted from beagles and fabricated into treated dentine matrix (TDM), according to a published process (Li et al., 2011). Then, DPEM and laminin-modified DPEM scaffolds were, respectively, placed into root-shaped TDM, and the composites were transplanted into the jaw of beagles for dental pulp regeneration.

In this study, one implant was implanted on the left and right sides of each dog’s mandible, and three beagles were used that were obtained from the Animal Research Centre of Dalian Medical University (Dalian, China). The treatments and the study protocol complied with all committee regulations approved by the Ethics Committee for Animal Experimentation of the Dalian Medical University.

**Isolation and Culture of Dental Pulp Stem Cells (DPSCs)**

**DPSCs Culture**

Human DPSCs were obtained from healthy wisdom teeth extracted for clinical purposes. Concretely, the teeth were transversely cut; then, the pulp tissues were aseptically collected from the dental pulp cavity. The pulp tissue was cut into small pieces and used for primary culture in Dulbecco’s modified Eagle’s medium (α-MEM, Hyclone, United States) supplemented with 10% fetal bovine serum (FBS, Hyclone, United States).
United States) in a humidified atmosphere at 37°C and 5% CO₂, following the procedure reported by Shigeta et al. (Takizawa et al., 2019). Cell culture medium was refreshed every 2 days. DPSCs from passages 3–6 were used in the experiments.

**Immunofluorescent (IF) Analysis**

To describe the characterization of the obtained DPSCs, mouse primary antibodies against Vimentin (1:200 dilution, Abcam, United States) and CK-14 (1:500 dilution, Abcam, United States) were used in IF staining. Briefly, cells samples were fixed in 10% formalin for 2 h, rinsed in PBS for 15 min and then 0.2% Triton X-100 for 30 min. Samples were then blocked with 1% albumin bovine serum (BSA, Solarbio, China) for 1 h at room temperature. Primary antibodies were applied in blocking buffer overnight at 4°C, followed by secondary antibody (Alexa Fluor 488/555 Goat anti Mouse) (Invitrogen, Carlsbad, CA, United States) at 1:500 dilution for 2 h at 37°C. Samples were counterstained using DAPI (1:1000 dilution, Sigma, United States) and images acquired using inverted fluorescent microscope (Leica Optical, Germany).

**Influences of Laminins on DPSCs**

**Cell Adhesion**

To observe the effect of laminins (1 mg/mL, L2020, Sigma, St. Louis, MO, United States) on cell adhesion, various concentrations of laminins were used in this study. Concretely, laminins were serially diluted in ultrapure distilled water to 0.1, 1, 10, and 100 μg/mL. Then, various concentrations of laminins were poured into enzyme-free sterile glass culture dishes (Supin, Nantong, China) and placed in an aseptic incubator with a humidified atmosphere at 37°C and 5% CO₂ for 2 days until the water was dried. The laminin-coated Petri dishes were obtained and seeded with DPSCs at a density of 6 × 10⁴/mL (culture media: 3 mL/well) in α-MEM supplemented with 10% FBS. A non-coated Petri dish was used as control in this experiment. Photographs of cells were taken using a phase contrast microscope (Olympus, Tokyo, Japan) at 1 and 24 h, respectively. To compare the number of cell adhesions at 24 h, three images were randomly selected and analyzed by ImageJ software (National Institutes of Health, Bethesda, MD, United States) for each group.

**Odontogenic Differentiation**

To analyze the influences of laminins on cells, real-time quantitative polymerase chain reaction (RT-qPCR) analysis was used in this study. Briefly, laminin solution was first diluted in culture medium to 100 μg/mL as experimental medium. Then, 1 × 10⁴ DPSCs were seeded and cultured in culture medium containing laminin or not. After 1 week of cell culture, total RNA was isolated using RNeasy Plus (TaKaRa, Japan) according to the manufacturer's instructions, followed by complementary DNA (cDNA) synthesis and PCR procedures. The cycling conditions were as follows: 95°C for 10 min, 45 cycles at 95°C (15 s each), and 60°C for 1 min. The data was analyzed by the 2⁻ΔΔCt method (Livak and Schmittgen, 2001). The primer sequences for analyzed genes are listed in Table 1.

**Fabrication and Biocompatibilities of Laminin-Modified DPEM**

**DPEM Fabrication**

To fabricate DPEM, the first and second incisor teeth, second and third molar tooth germs (M2 and M3, respectively) were obtained from the recently discarded swine jaws as in our previous report (Chen et al., 2015a). Dental pulp tissues were peeled off from the obtained tooth and rinsed thoroughly in phosphate buffer solution (PBS, Solarbio, China). Then, the prepared dental pulp tissues were treated according to a decellularization process (Ma et al., 2013). Concretely, the dental pulp tissues were incubated in 1% SDS (Bio-Rad, United States) for 12 h, followed by 30 min of 1% Triton X-100 (Sigma, United States) in deionized water. After decellularization, the sterilization of DPEM was performed by washing DPEM in PBS for 30 min, followed by immersing it in a solution containing 100 units/ml penicillin (Hyclone, United States) and 100 mg/ml streptomycin (Hyclone, United States) for 48 h (Ott et al., 2008).

**Laminin-Modified DPEM Fabrication**

To obtain the laminin-modified DPEM, laminin (1 mg/mL, L2020, Sigma, St. Louis, MO, United States) purified from the basement membrane of Engelbreth–Holm swarm murine sarcoma was diluted in ultra-pure distilled water to 100 μg/mL (Rajabi et al., 2018). Then, the fabricated DPEM (10 mm × 5 mm × 3 mm) was directly coated with 100 μg/mL.

**Table 1 | Oligonucleotide primer sequences.**

| Target cDNA | Primer sequence (5'-3') | Product size (bp) | NCBI no. |
|-------------|-------------------------|-------------------|----------|
| GAPDH       | F CCATCTTTCAGGACGAGAATCR CCCCAGCTCTTCCATGTTG | 105 | NM_001289746 |
| DLK-5       | F CAACAGGCAAGAGAAGATGAR GGGGAACGGAGATGACTGAGT | 118 | NM_0052216 |
| SP7         | F AGGGCCCTGTGCTGTGCAATCR GTTGGCCTGCTGGTTTTGCT | 117 | NM_001734673 |
| COL-2       | F GAGAGACTCTGGAGACGAGAAR GTGGAACAGAGCCGCTGAA | 119 | NM_0018444 |
| COL-10      | F TGGTCTGGCTTATAAGAATGCR GCAATTTGACTCGGTGGCT | 117 | NM_000493 |
| MMP13       | F GAGACCTTGAGACACTCTGATR CATTCTTGCGCTGTTTGTCA | 119 | NM_0022473 |
| DSPP        | F AGAGAACAAATTGGACAGCGCAAGAR CTGGTGACGGACCGTTGATT | 116 | NM_0142083 |
| ALP         | F AAGCTGTGCTGCTGTGCAATCR GCAATTTGACTCGGTGGCT | 118 | NM_0030644 |
| RUNX2       | F CGTGGCTGTCAAGTGCTGTGCAATCR GCAATTTGACTCGGTGGCT | 117 | NM_00105051 |
| MSX2        | F CGCGCGCGCAAGACATGCR TGCGACCTGCTGGATGGA | 120 | NM_0024495 |
laminin solutions for 2 h at 37°C. After that, laminin-modified DPEM were prepared for use in this study.

**IF Analysis**

To detect the cell nucleuses in DPEM, 2-(4-Aminophenyl)-6-indolecarbamidine dihydrochloride (DAPI) (1:1000 dilution, Sigma, United States) staining was used. The samples were prepared according to the previous report (Chen et al., 2015a). Tissue sections (5 μm) were mounted using DAPI-containing mounting media for 3 min and observed by inverted fluorescent microscope (Leica Optical, Germany).

To observe the distribution of laminins, the tissue sections of DP, DPEM, and laminin-modified DPEM were prepared to detect the expressions of laminin (1:250 dilution, Abcam, United States). After DPSCs were seeded on the surface of laminin-modified DPEM for 1 week, the tissue sections of laminin-modified DPEM/cells were prepared to test the persistency of laminins. IF analysis was used in these two experiments.

**Scanning Electron Microscope (SEM) Analysis**

To observe the effects of laminin on cell proliferation, SEM was used to observe the cells on DPEM and laminin-modified DPEM. Briefly, the same number of DPSCs were seeded on DPEM and laminin-modified DPEM for 1 week. DPEM and DP as control samples were prepared. Then, the four samples were prefixed by immersion in 2% glutaraldehyde in 0.1 M PBS, and postfixed for 2 h in 1% osmic acid dissolved in PBS. Samples were then treated in a graded series of ethanol and t-butyl alcohol, dried in a freeze dryer (ES-2030, Hitachi, Tokyo, Japan), platinum-coated using an ion coater (IB-3, Eiko, Japan), and observed under SEM (ZEISS, Germany).

**In situ Jawbone Transplantation in Beagle Dogs**

All animal experiments described in this study were conducted in accordance with protocols approved by the Ethics Committee of Dalian Medical University. The beagles (8–12 kg) were purchased from the Laboratory Animal Center of Dalian Medical University (Dalian, China).

**Preparation of Dental Pulp Cavity**

To simulate the morphology of the dental pulp cavity, the TDM were fabricated and used in the dental pulp cavity for dental pulp regeneration in this study. Briefly, we harvested the extracted teeth from beagles and then removed the crown, dental pulp, predentin, and cementum using a mechanical method (Li et al., 2011). Finally, the dentin matrix was treated with 17% ethylenediaminetetraacetic acid (EDTA, Sigma, United States) for 12 min, 10% EDTA for 12 min, and 5% EDTA for 20 min. For sterilization, TDM was immersed in sterile PBS supplemented with 100 units/ml penicillin and 100 mg/ml streptomycin for 24 h in 37°C, then washed with sterile deionized water for 10 min in an ultrasonic cleaner and finally stored in α-MEM at 4°C.

**Transplantation**

Three beagles had their second premolars removed before transplantation. ECM materials (DPEM, laminin-modified DPEM, n = 3) combined with TDM as composites for dental pulp regeneration were prepared and transplanted into the extraction wound of the second premolar. The surgical procedure was performed under deep anesthesia.

**CBCT Analysis and Histology Analysis**

Beagles were sacrificed after 12 weeks, and the mandibles were harvested and fixed with 4% paraformaldehyde. Cone-beam computed tomography (CBCT, Vatech, South Korea) was used to observe the harvested samples. All samples were then dehydrated for 1 month, embedded, and sectioned into 5-μm-thick sections for histological analyses according to the manufacturer’s recommended protocols. As mentioned earlier, the prepared sections (5 μm) were also stained with H&E stain. For immunohistochemistry analysis, the primary antibodies used in this study were as follows: rabbit anti-DSP (1:100 dilution; Abcam, MA, United States), rabbit anti-collagen type I (Col-1, 1:200 dilution, Bioss, Inc., Woburn, MA, United States), rabbit anti-laminin (1:50 dilution, Abcam, MA, United States), rabbit anti-DMP-1 (1:50 dilution, Invitrogen, Eugene, OR, United States).

**RESULTS**

**Isolation and Culture of DPSCs**

Primary DPSCs were successfully obtained from the dental pulp of the impacted tooth as in our previous reports (Chen et al., 2015a). From passage 1 (P1) to 5 (P5), the cells kept the typical spindle morphology of mesenchymal cells (Figure 2A) and maintained a good state of proliferation. Meanwhile, IF staining revealed that the cells were positive for mesenchymal cell marker vimentin (Figure 2B) and negative for epithelial cell marker CK-14 (Figure 2C).

**Influences of Laminins on DPSCs**

**Cell Adhesion**

To investigate the effects of laminins on cell adhesion, laminins were coated on plates at concentrations of 0.1 (laminin-0.1), 1 (laminin-1), 10 (laminin-10), and 100 μg/mL (laminin-100). The results showed that most cells in all the groups remained spherical in shape. However, we found that some cells started attaching and forming protrusions in the laminin-100 group (Figure 3A). After being co-cultured for 24 h, the adherent cells were spindle-shaped and flat in all groups (Figure 3B), whereas the number of cells in the laminin-100 group was the highest in all groups. The histogram showed that the number in the laminin-100 group was statistically higher than the blank group, which demonstrated laminins at the concentration of 100 μg/mL could promote cell adhesion significantly (Tang and Saito, 2018).

**Odontogenic Differentiation**

To investigate the odontogenic influences of laminins on DPSCs, DPSCs were co-cultured with laminins at a concentration of 100 μg/mL for 1 week. Real-time PCR revealed increased expression of relative quantification to the early odontogenic
genes, alkaline phosphatase (ALP) (nearly 13.5-fold higher than the control group), muscle segment homeodomain homeobox 2 (MSX2) (3.5-fold), collagen type X alpha 1 (COL-10) (4.3-fold), and matrix metallopeptidase 13 (MMP13) (7.9-fold). The expression of other osteogenic/odontogenic markers, such as distal-less homeobox 5 (DLX5), dentin sialophosphoprotein (DSPP), Runt-related transcription factor 2 (RUNX2), and Sp7 transcription factor (SP7), did not change significantly. Meanwhile, laminins downregulated the expression of cartilage-specific gene collagen type II alpha 1 (COL-2) (minus 10.0-fold) (Figure 4).

Characterization of Laminin-Modified DPEM

DPEM

The obtained developing tooth from swine with rich, highly vascularized, reddish-colored, dental pulp tissues (Figure 5A). After decellularization, the fabricated DPEM appeared white as compared to DP but preserved the predetermined size and shape of dental pulp tissues. Meanwhile, DAPI staining showed the absence of cell nuclei in DPEM specimens, indicating complete decellularization (Figure 5B) as compared to native DP.

Laminin Coating Persistency

The expression patterns of laminin in DP, DPEM, and DPEM/LN materials were tested utilizing IF staining (Figure 5C). The DP presented strong fluorescent signals in the BM of vascular structures and the odontoblast layer (Figure 5C: DP). After decellularization, laminins at the BM of vascular structures were preserved but lost at the place of the odontoblast layer in DPEM (Figure 5C: DPEM), consistent with the published reports (Chen et al., 2015a). Alexa Fluor 488-coupled laminin coating, a continuous, bright green fluorescence, was presented along the surface of laminin-modified DPEM (Figure 5C: DPEM/LN), meaning the method of laminin coating referred to previous reports (Toshmatova et al., 2019) would be feasible to the fabrication of laminin-modified DPEM.

When DPSCs were seeded on laminin-coated DPEM for 1 week, the fluorescence still could be detected though the intensity was visually reduced (Figure 5C: DPEM/LN/cell +).

SEM Analysis

Scanning electron microscope images demonstrated that the microstructure of dental pulp tissues possessed a dense surface (Figure 5D: DP), but the decellularized dental pulp tissues (Figure 5D: DPEM) presented a loose and porous
In our previous report (Chen et al., 2015a). Then, DPEM/TDM and DPEM/LN/TDM composites were separately implanted into alveolar sockets (Figure 6C). After 12 weeks, CBCT images showed the harvested implants without obvious immune rejection and severe inflammatory reaction (Figures 6D,G), indicating the good biocompatibility of implant biomaterials. H&E staining verified that the cellular cementum/bone-like structures and blood vessels were regenerated obviously in the DPEM-alone group (Figures 6E,F). Thus, DPEM could be revascularized effectively to nourish the dentine tissues (Chen et al., 2015a). In the DPEM/LN group, odontoblastic layer-like structures were observed on the interface between dental pulp–like tissues and the dentin matrix (Figures 6H,I).
FIGURE 4 | The odontogenic influences of laminin on DPSCs. After 1 week, DPSCs co-cultured with laminins at the concentration of 100 µg/mL upregulated the early odontogenic markers, ALP, MSX2, Col-10, and MMP13. However, laminins did not change the expression of other osteogenic/odontogenic markers, such as DLX5, DSPP, RUNX2, and SP7. Meanwhile, laminins downregulated the expression of cartilage-specific gene Col-2.

* p < 0.05, **p < 0.01, ***p < 0.001, NS means no significance.

Immunohistochemistry was used to evaluate the regenerated pulp-like tissue (Figure 7). The results showed that the generated odontoblastic layer-like structures in DPEM/LN group were positive for the related odontogenic markers, Col-1 (Figures 7A,a), DMP-1 (Figures 7B,b), DSPP (Figures 7C,c), and LN (Figures 7D,d), which were similar to the expression patterns of native dental pulp tissues (Figures 7K–N). The harvested DPEM group regenerated the cellular cementum/bone-like structures (Figures 7F–I). As a negative control, the harvested samples were negative for PBS (Figures 7E,J,O).

DISCUSSION

In the present study, we describe the amelioration of DPEM by incorporation of laminins, aiming at the formation of a continuous odontoblast layer in dental pulp regeneration. DPEM as a unique and effective scaffold has been obtained and utilized for dental pulp regeneration (Zhang et al., 2017). However, associated with decellularization, one main challenge is that partial ECM components are often stripped away or altered by the detergents used to remove cellular debris (Young et al., 2019). Thus, the loss of ECM components may affect the effect of DPEM on dental pulp regeneration.

Laminins, as effective biological molecules, were lost partially in fabricated DPEM (Chen et al., 2015a), which could control odontoblast proliferation and differentiation through engaging several integrin receptors of cell surfaces or growth factors (Tang and Saito, 2018). In in vitro culture, there were the highest number of adherent DPSCs in the laminin-100 group (Figure 3B). It demonstrated that 100 µg/mL laminins could contribute to mesenchymal cell adhesion in dental implants (Min et al., 2013). Actually, except for promoting the cell adhesion, the influence of laminins on the osteo/odontoblastic differentiation was also evaluated in this study. The expressions of related odontogenic genes were assessed by RT-PCR in this study (Figure 4). The results showed that ALP was upregulated nearly 13.5-fold higher than the control group (Figure 4), which is an early marker of odonto/osteoblast differentiation. The previous report demonstrates that laminins could activate the ALP activity of an odontoblast-like cell line (Tang and Saito, 2017). Thus, the enhancement of ALP in the present study denotes that laminins can promote the DPSC differentiation process toward mineralizing tissue (Tang and Saito, 2017). Meanwhile, Mx2 homeoprotein, a key transcription factor of dental and periodontal tissue formation (Fujii et al., 2015), was also upregulated about 3.5-fold higher than control group (Figure 4). In a previous report, Towler DA et al. detected the expression of Mx2 in ovoid pre-odontoblasts (Bidder et al., 1998). It is involved in many molecular pathways controlling mineralized tissue homeostasis, such as the Wnt/sclerostin pathway (Korah et al., 2019). In our study, the expression of Col-10 was upregulated nearly 4.3-fold (Figure 4). During the stages of ECM protein secretion and mineralization, Col-10 genes are expressed in mesenchymal cells of developing teeth and are involved in odontogenic differentiation (Debiais-Thibaud et al., 2019). MMP-13 is a member of the zinc-dependent endopeptidases...
FIGURE 5 | Fabrication and characterization of laminin-modified DPEM. The panel (A) shows the obtained developing tooth from swine with rich dental pulp tissues (DP). After the process of decellularization, the fabricated DPEM preserved the predetermined size and shape of dental pulp tissues. The cells in DP were not visualized in DPEM (B) by staining nuclei with the fluorescent dye DAPI. The panel (C) shows a continuous, brightly green fluorescence (LN-bound Alexa 488) along the surface of LN-coated graft but not on the surface of DPEM. Meanwhile, after being seeded with DPSCs for 1 week, DPEM/LN shows the persistency of LN coating though the intensity was visually reduced. For further observation, SEM analysis (D) was used to observe the microstructure of DP and DPEM. After cell seeding for 1 week, the SEM images of laminin-modified DPEM (DPEM/LN) showed better cell viability than DPEM. DPEM, dental pulp extracellular matrix; DPEM/LN, laminin-modified DPEM; DP, dental pulp; Yellow scale bars: 1 cm; White scale bars: 200 μm.

playing an important role during ECM formation. The expression of MMP-13 in DPSCs has been upregulated nearly 7.9-fold in the laminin group (Figure 4). It has been demonstrated that mature human odontoblasts could express MMP-13 (Nurmenniemi et al., 2010). The MMP-13 expression is mediated via activation of the ERK and NF-κB signal pathways in odontoblasts, involved in remodeling of the pulp-dentine complex (Zhang et al., 2013).

Meanwhile, for the four genes, DLX5, DSPP, RUNX2, and SP7, there was no significant change of expression in the laminin group compared with control (Figure 5). RUNX2, as one specific osteoblast transcription factor, was slightly decreased in this study. COL-2, as one cartilage-specific gene, was inhibited significantly (Figure 5). The expression of both RUNX2 and COL-2 suggest commitment into an odontoblastic phenotype as opposed to osteoblastic (Farshdousti Hagh et al., 2015) or chondroblastic phenotype (Agrawal and Pramanik, 2019). DLX5, as one non-specific osteoblast transcription factor (Lee et al., 2013), can form a heterodimer with Mxs2 regulating common target genes, which includes osteocalcin, bone sialoprotein, osteopontin, and collagen type I alpha1 (Farshdousti Hagh et al., 2015). DSPP was slightly increased in this study, which was a typical factor in odontoblasts of the pulp-dentin complex
Orthotopic implantation for dental pulp regeneration. The extracted tooth (A) from beagles were fabricated into treated dentin matrix (TDM) (B), which could provide a large enough pulp cavity for dental pulp regeneration. Then, DPEM/TDM and DPEM/LN/TDM were separately implanted into alveolar sockets (C). After 12 weeks, CBCT showed the harvested samples at the implant sites (D,G). H&E staining verified that the cellular cementum/bone-like structures were regenerated obviously in the DPEM group (E,F). In the DPEM/LN group, odontoblastic layer-like structures were generated on the interface between dental pulp–like tissues and dentin matrix (H,I). (The yellow arrow labels the implant; the red arrows label the generated vessels in dental pulp tissues and the green arrows label the odontoblastic layer). TDM, treated dentine matrix; DPEM, dental pulp extracellular matrix; DPEM/LN, laminin-modified DPEM; DP, dental pulp. d, dentin matrix; b, bone-like tissues; o, odontoblastic layer. Scale bars: 200 µm.

Sp7, a zinc finger transcription factor, could coordinately modulate RUNX2 and DLX5 proteins at levels appropriate for optimal osteo/odontoblastic differentiation and function (Barone et al., 2014). Based on the slight increment of DSPP and Sp7 expression, we speculate that additional mineralized microenvironments may be required in in vitro culture (Yuasa et al., 2004; Tang et al., 2018).

Diverse methods, such as physical coating, covalent chemical bonding, and blended electrospinning have been employed to immobilize laminin protein on the surfaces of substrates (Koh et al., 2008). In the present study, we fabricated laminin-modified DPEM based on the physical coating strategy (Figure 5). The fluorescence of laminin still could be detected on the surface of the scaffold even after being seeded and cultured in vitro for 1 week (Figure 5C), showing the good persistence of laminin coating. Payam Akhyari et al. demonstrated the physical coating of laminin could persist on decellularized grafts for at least 8 weeks in vivo (Toshmatova et al., 2019). Meanwhile, SEM results showed DPSCs presented multilayer growth on the surface of the laminin-coated DPEM (Figure 5D). Therefore, the above results demonstrated that the physical coating of laminin could functionalize the DPEM surface to improve the adhesion of DPSCs. This observation is in accordance with the reported result that the laminin-coated surface could provide the functional biochemical signals for enhancing cell attachment and proliferation (Nie et al., 2018).

The in vivo transplantation is the “gold standard” to verify the validity of one strategy for tissue regeneration. Cell transplantation (Zhu et al., 2018) and cell homing (Kim et al., 2010), as two strategies, have been applied in dental pulp regeneration. The difference between the two strategies is the requirement of exogenous stem cells as seed cells. The cell homing strategy without the requirement for exogenous stem cells may avoid difficulties in obtaining regulatory approval, stem cell isolation and processing, the relatively high cost associated with cell cryopreservation, expansion, and a biological risk of immune-rejection, infection, and tumorigenesis (Kim et al., 2013). Thus, in this study, laminin-modified DPEM combined with TDM—one cell-free strategy was investigated for dental pulp regeneration in vivo.
Whatever the pulp-regeneration strategy, the regenerated tissues in root canals after the application of clinical regeneration protocols seem to be of periodontal origin as evinced by the presence of periodontal ligament-like, cementum-like, bone-like tissues (Kim, 2017). Laminin-modified DPEM combined with TDM (Figures 6A,B) were transplanted into the mandibles of beagles for 12 weeks. Odontoblastic layer-like structures were observed on the interface between dental pulp-like tissues and dentin matrix (Figures 6H,I) in the DPEM/laminin group. In contrast, the cellular cementum/bone-like structure was regenerated obviously in the DPEM-alone group (Figures 6E,F). Thus, the laminin coating may be useful to provide the support and functional biochemical signals for diverting the cellular events toward pulp-dentin complex regeneration rather than cementum-like tissue repair (Kim, 2017).

Meanwhile, DSPP and DMP-1 are the two most frequently used markers for odontoblastogenesis (Chen et al., 2015b), and laminins are widely expressed in tooth BM (Yuasa et al., 2004). DSPP, DMP-1 as well as laminin were positive in the generated odontoblastic layer-like structures verifying the generation of the odontoblastic layer (Figure 7). However, laminins showed limited capacity in inducing DSPP expression in in vitro culture (Figure 5; Tang et al., 2018), but DSPP was positive in in vivo results (Figure 7). The possible explanation is that a single growth factor cannot construct a complete odontogenic microenvironment, which requires the participation of laminin, DPEM, and TDM.

**CONCLUSION**

In conclusion, we successfully fabricated laminin-modified DPEM and illustrated the roles of laminins in odontogenic differentiation in vitro. Meanwhile, the present study shows the effects of laminins on the generation of an odontoblast layer and provides a feasible strategy for the
regeneration of dental pulp tissues. However, it is necessary to further explore an appropriate preservation for laminin-modified DPEM to facilitate clinical use.

**DATA AVAILABILITY STATEMENT**

The datasets presented in this study can be found in online repositories. The names of the repository/repositories and accession number(s) can be found below:

https://www.ncbi.nlm.nih.gov/, NM_00289746; https://www.ncbi.nlm.nih.gov/, NM_0043355; https://www.ncbi.nlm.nih.gov/, NM_00173467.3; https://www.ncbi.nlm.nih.gov/, NM_001844.4; https://www.ncbi.nlm.nih.gov/, NM_003064.4; https://www.ncbi.nlm.nih.gov/, NM_000493.4; https://www.ncbi.nlm.nih.gov/, NM_002449.5.

**ETHICS STATEMENT**

The studies involving human participants were reviewed and approved by the Ethics Committee of the First Affiliated Hospital of Dalian Medical University. The patients/participants provided their written informed consent to participate in this study. The animal study was reviewed and approved by the Ethics Committee for Animal Experimentation of the Dalian Medical University.

**AUTHOR CONTRIBUTIONS**

GC: designing experiments and supervision. JF and JC: writing – original draft preparation and data curation. WL, XY, and HQ: animal surgery, scaffold preparation, and evaluation. JY: writing, reviewing, and editing. JF and WL: histological evaluation, cell isolation, and culture. All authors contributed to the article and approved the submitted version.

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**REFERENCES**

Agrawal, P., and Pramanik, K. (2019). Enhanced chondrogenic differentiation of human mesenchymal stem cells in silk fibroin/chitosan/glycosaminoglycan scaffolds under dynamic culture condition. *Differentiation* 110, 36–48. doi: 10.1016/j.diff.2019.09.004

Aumailley, M. (2013). The laminin family. *Cell Adh. Migr.* 7, 48–55. doi: 10.4161/cam.22826

Barone, A., Toti, P., Funel, N., Campani, D., and Covani, U. (2014). Expression of SP7, RUNX1, DLX5, and CTNNB1 in human mesenchymal stem cells cultured on xenogenic bone substitute as compared with machined titanium. *Implant Dent.* 23, 407–415.

Biddler, M., Latifi, T., and Towler, D. A. (1998). Reciprocal temporospatial patterns of Msx2 and Osteocalcin gene expression during murine odontogenesis. *J. Bone Miner Res.* 13, 609–619. doi: 10.1359/bmr.1998.13.4.609

Chen, G., Chen, J., Yang, B., Li, L., Luo, X., Zhang, X., et al. (2015a). Combination of aligned PLLA/Gelatin electrospun sheets, native dental pulp extracellular matrix and treated dentin matrix as substrates for tooth root regeneration. *Biomaterials* 52, 56–70. doi: 10.1016/j.biomaterials.2015.02.011

Chen, G., Sun, Q., Xie, L., Jiang, Z., Feng, L., Yu, M., et al. (2015b). Comparison of the odontogenic differentiation potential of dental follicle, dental papilla, and cranial neural crest cells. *J. Endod.* 41, 109–1099. doi: 10.1016/j.joen.2015.03.003

Debiais-Thibaud, M., Simion, P., Venteo, S., Munoz, D., Marcellini, S., Mazan, S., et al. (2019). Skeletal mineralization in association with Type X collagen expression is an ancestral feature for jawed vertebrates. *Mol. Biol. Evol.* 36, 2265–2276. doi: 10.1093/molbev/msz145

Eramo, S., Natali, A., Pinna, R., and Milia, E. (2018). Dental pulp regeneration via farshdousti Hagh, M., Noruzinia, M., Mortazavi, Y., Soleimani, M., Kaviani, S., Abroun, S., et al. (2015). Different methylation patterns of RUNX2, OSX, DLX5 and BSP in osteoblastic differentiation of mesenchymal stem cells. *Cell J.* 17, 71–82.

Fuji, S., Fujimoto, K., Goto, N., Kanawa, M., Kawamoto, T., Pan, H., et al. (2015). Characteristic expression of MSX1, MSX2, TBX2 and ENTPD1 in dental pulp cells. *Biomed. Res.* 3, 566–572. doi: 10.3892/br.2015.456

Gilpin, S. E., and Ott, H. C. (2015). Using nature's platform to engineer bio-artificial lungs. *Ann. Am. Thorac. Soc.* 12(Suppl. 1), S43–S49.

Guo, T., Cao, G., Liu, B., Li, Z., and Chen, W. (2019). Olfalphi1 hinders autophagy by DSP upregulation in odontoblast differentiation. *Int. J. Biochem. Cell Biol.* 115:105578. doi: 10.1016/j.biocel.2019.105578

Hu, L., Gao, Z., Xu, J., Zhu, Z., Fan, Z., Zhang, C., et al. (2017). Decellularized swine dental pulp as a bioscaffold for pulp regeneration. *Biomol. Res. Int.* 2017:9342714.

Hyres, R. O. (2009). The extracellular matrix: not just pretty fibrils. *Science* 326, 1216–1219. doi: 10.1126/science.1176009

Kawashima, N., and Okiji, T. (2016). Odontoblasts: specialized hard-tissue-forming cells in the dentin-pulp complex. *Congenit. Anom.* 56, 144–153. doi: 10.1111/cga.12169

Kim, J. Y., Xin, X., Moioli, E. K., Chung, J., Lee, C. H., Chen, M., et al. (2010). Regeneration of dental-pulp-like tissue by chemotaxis-induced cell homing. *Tissue Eng. Part A* 16, 3023–3031. doi: 10.1089/ten.tea.2010.0181

Kim, S. G. (2017). Biological molecules for the regeneration of the pulp-dentin complex. *Dent. Clin. North Am.* 61, 127–141. doi: 10.1016/j.dcn.2016.08.005

Kim, S. G., Zheng, Y., Zhou, J., Chen, M., Embree, M. C., Song, K., et al. (2013). Dentin and dental pulp regeneration by the patient's endogenous cells. *Endod. Top.* 28, 106–117. doi: 10.1111/etp.12037

Koh, H. S., Yong, T., Chan, C. K., and Ramakrishna, S. (2008). Enhancement of neurite outgrowth using nano-structured scaffolds coupled with laminin. *Biomaterials* 29, 3574–3582. doi: 10.1016/j.biomaterials.2008.05.014

Korah, L., Amri, N., Bugueno, I. M., Hotton, D., Tenenbaum, H., Huck, O., et al. (2019). Experimental periododontitis in Msx2 mutant mice induces alveolar bone necrosis. *J. Periodontol.* 91, 693–704. doi: 10.1002/jpe.16-0435

Lee, J., Corcoran, A., Han, M., Gardiner, D. M., and Muneoka, K. (2013). DLX5 and Msx2 regulate mouse anterior neural tube closure through ephrinA5-EphA7. *Development* 140, 341–349. doi: 10.1242/dev.12044

Li, R., Guo, W., Yang, B., Guo, L., Sheng, L., Chen, G., et al. (2011). Human swine dental pulp as a bioscaffold for pulp regeneration. *Biomed. Res. Int.* 2011:934271.

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regeneration. *Biomaterials* 32, 4525–4538. doi: 10.1016/j.biomaterials.2011.03.008
Livak, K. J., and Schmittgen, T. D. (2001). Analysis of relative gene expression data using real-time quantitative PCR and the 2(-Delta Delta C(T)) Method. *Methods* 25, 402–408. doi: 10.1006/meth.2001.1262
Ma, R., Li, M., Luo, J., Yu, H., Sun, Y., Cheng, S., et al. (2013). Structural integrity, ECM components and immunogenicity of decellularized laryngeal scaffold with preserved cartilage. *Biomaterials* 34, 1790–1798. doi: 10.1016/j.biomaterials.2012.11.026
Martino, M. M., Briquez, P. S., Guc, E., Tortelli, F., Kilarski, W. W., Metzger, S., et al. (2014). Growth factors engineered for super-affinity to the extracellular matrix enhance tissue healing. *Science* 343, 885–888. doi: 10.1126/science.1247863
Min, S. K., Kang, H. K., Jang, D. H., Jung, S. Y., Kim, O. B., Min, B. M., et al. (2013). Titanium surface coating with a laminin-derived functional peptide promotes bone cell adhesion. *Biomed. Res. Int.* 2013:638348.
Nie, Y., Wang, W., Xu, X., Zou, J., Bhuvanesh, T., Schulz, B., et al. (2018). Titanium surface coating with a laminin-derived functional peptide promotes bone cell adhesion. *Biomed. Res. Int.* 2013:638348.
Ornell, J. D., Anfang, R., Anandappa, A., Costa, J., Javidfar, J., Wobma, H. M., et al. (2010). Toll-like receptor 9 ligands enhance mesenchymal stem cell invasion and expression of matrix metalloprotease-13. *Exp. Cell Res.* 316, 2676–2682. doi: 10.1016/j.yexcr.2010.05.024
O’Neill, J. D., Anfang, R., Anandappa, A., Costa, J., Javidfar, J., Wobma, H. M., et al. (2013). Decellularization of human and porcine lung tissues for pulmonary tissue engineering. *Ann. Thorac. Surg.* 96, 1046–1055. discussion 1055-6. doi: 10.1016/j.thorsurg.2013.04.022
Ott, H. C., Matthiesen, T. S., Goh, K. S., Black, L. D., Kren, S. M., Netoff, T. I., et al. (2008). Perfusion-decellularized matrix: using nature’s platform to engineer a bioartificial heart. *Nat. Med.* 14, 213–221. doi: 10.1038/nm1684
Paduano, F., Marrelli, M., Alom, N., Amer, M., White, L. J., Shakesheff, K. M., et al. (2017). Decellularized bone extracellular matrix and human dental pulp stem cells as a construct for bone regeneration. *J. Biomat. Sci. Polym. Ed.* 28, 730–748. doi: 10.1080/09205063.2017.1301770
Rajabi, M., Firouzi, M., Hassannejad, Z., Haririan, I., and Zahedi, P. (2018). Titanium surface coating with a laminin-derived functional peptide promotes bone cell adhesion. *Biomed. Res. Int.* 2013:638348.
Rajiabi, M., Firouzi, M., Hassannejad, Z., Haririan, I., and Zahedi, P. (2018). Fabrication and characterization of electropspun laminin-functionalized silk fibroin/poly(ethylene oxide) nanofibrous scaffolds for peripheral nerve regeneration. *J. Biomed. Mater. Res. B Appl. Biomater.* 106, 1595–1604. doi: 10.1002/jbmr.b.33968
Sutherland, A. J., Beck, E. C., Dennis, S. C., Converse, G. L., Hopkins, R. A., Berkland, C. J., et al. (2015). Decellularized cartilage may be a chondroinductive material for osteochondral tissue engineering. *PloS One* 10:e0121966. doi: 10.1371/journal.pone.0121966
Takizawa, S., Yamamoto, T., Honjo, K. I., Sato, Y., Nakamura, K., Yamamoto, K., et al. (2019). Transplantation of dental pulp-derived cells cultured on human amniotic membrane induced to differentiate into bone. *Oral. Dis.* 25, 1352–1362. doi: 10.1111/odi.13096
Tang, J., and Saito, T. (2017). Human plasma fibronectin promotes proliferation and differentiation of odontoblast. *J. Appl. Oral. Sci.* 25, 299–309. doi: 10.1590/1678-7757-2016-0442
Tang, J., and Saito, T. (2018). Laminin-1 acts as an adhesive for odontoblast-like cells and promotes their differentiation toward a hard tissue-forming phenotype. *J. Oral. Sci.* 60, 253–261. doi: 10.2334/josnusd.17-0286
Tang, J., Saito, T., and Novel Fragment, A. (2018). Derived from Laminin-411 facilitates proliferation and differentiation of odontoblast-like cells. *Biomed. Res. Int.* 2018:9456383.
Toshmatova, M., Nakanishi, S., Sugimura, Y., Schmidt, V., Lichtenberg, A., Assmann, A., et al. (2019). Influence of laminin coating on the autologous in vivo recellularization of decellularized vascular protheses. *Materials* 12:3351. doi: 10.3390/ma12203351
Uyygen, B. E., Soto-Gutierrez, A., Yagi, H., Izamis, M. L., Guzzardi, M. A., Shulman, C., et al. (2010). Organ reengineering through development of a transplantable recellularized liver graft using decellularized liver matrix. *Nat. Med.* 16, 814–820. doi: 10.1038/nm.2170
Xuan, K., Li, B., Guo, H., Sun, W., Kou, X., He, X., et al. (2018). Deciduous autologous tooth stem cells regenerate dental pulp after implantation into injured teeth. *Sci. Transl. Med.* 10:eaa3227. doi: 10.1126/scitranslmed.aas3227
Yap, L., Tay, H. G., Nguyen, M. T. X., Tjin, M. S., and Tryggvason, K. (2019). Laminins in cellular differentiation. *Trends Cell Biol.* 29, 987–1000. doi: 10.1016/j.tcb.2019.10.001
Young, B. M., Shankar, K., Tho, C. K., Pellegrino, A. R., and Heise, R. L. (2019). Laminin-driven Epac/Rap1 regulation of epithelial barriers on decellularized matrix. *Acta Biomater.* 100, 223–234. doi: 10.1016/j.actbio.2019.10.009
Yuasa, K., Fukushima, S., Kanasaki, Y., Yamada, A., Fukushima, E., Kanaoka, K., et al. (2004). Laminin alpha2 is essential for odontoblast differentiation regulating dentin sialoprotein expression. *J. Biol. Chem.* 279, 10286–10292. doi: 10.1074/jbc.m310013200
Zhang, J., Zhu, Q. L., Huang, P., Yu, Q., Wang, Z. H., Cooper, P. R., et al. (2013). CpG ODN-induced matrix metalloproteinase-13 expression is mediated via activation of the ERK and NF-kappaB signalling pathways in odontoblast cells. *Int. Endod. J.* 46, 666–674. doi: 10.1111/iej.12043
Zhang, W., Vazquez, B., Oreadi, D., and Yelick, P. C. (2017). Decellularized tooth bud scaffolds for tooth regeneration. *J. Dent. Res.* 96, 516–523. doi: 10.1177/0022034516689082
Zhou, J., Fritze, O., Schleicher, M., Wendel, H. P., Schenke-Layld, K., Harasztosi, C., et al. (2010). Impact of heart valve decellularization on 3-D ultrastructure, immunogenicity and thrombogenicity. *Biomaterials* 31, 2549–2554. doi: 10.1016/j.biomaterials.2009.11.088
Zhu, X., Liu, J., Yu, Z., Chen, C. A., Aksel, H., Azim, A. A., et al. (2018). Model for stem-cell based de novo regeneration of dental pulp and dentin-like tissue. *Tissue Eng. Part C Methods* 24, 108–120. doi: 10.1089/tenc.tec.2017.0342

**Conflict of Interest:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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