Evaluation of 3D printed microfluidic networks to study fluid flow in rocks

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Abstract. Visualizing fluid flow in porous media can provide a better understanding of transport phenomena at the pore scale. In this regard, transparent micromodels are suitable tools to investigate fluid flow in porous media. However, using glass as the primary material makes them inappropriate for predicting the natural behavior of rocks. Moreover, constructing these micromodels is time-consuming via conventional methods. Thus, an alternative approach can be to employ 3D printing technology to fabricate representative porous media. This study investigates fluid flow processes through a transparent microfluidic device based on a complex porous geometry (natural rock) using digital-light processing printing technology. Unlike previous studies, this one has focused on manufacturing repeatability. This micromodel, like a custom-built transparent cell, is capable of modeling single and multiphase transport phenomena. First, the tomographic data of a carbonate rock sample is segmented and 3D printed by a digital-light processing printer. Two miscible and immiscible tracer injection experiments are performed on the printed microfluidic media, while the experiments are verified with the same boundary conditions using a CFD simulator. The comparison of the results is based on Structural Similarity Index Measure (SSIM), where in both miscible and immiscible experiments, more than 80% SSIM is achieved. This confirms the reliability of printing methodology for manufacturing reusable microfluidic models as a promising and reliable tool for visual investigation of fluid flow in porous media. Ultimately, this study presents a novel comprehensive framework for manufacturing 2.5D realistic microfluidic devices (micromodels) from pore-scale rock images that are validated through CFD simulations.

1 Introduction

Microfluidic systems are usually used in multidisciplinary studies to simulate transport processes and reveal relevant underlying mechanisms in details in porous media, and petroleum industry is not an exception [1-3]. These microfluidic networks, also known as fluidic micromodels, are employed to visualize fluid flow through porous-like networks. Manufacturing microfluidic-channels are mostly based on subtractive and additive fabrication methods [4].

Micromodels have been manufactured directly using glass beads in the Hele-Shaw flow approach [5] or by etching pore morphology on glasses/silicon wafers [6-8]. For example, Meisenheimer et al. [9] used a simplified porous medium of soda-lime glass beads to investigate two-phase flow. To etch the flow pattern on a siliceous glass, either laser-etching technique or wet etching approach can be implemented where laser beam (e.g., a CO2 laser device [10]) and acid is used respectively on silicon or silicon plates to develop microfluidic patterns [11]. In both approaches, a second glass plate is placed on top of the etched glass to create an enclosed pore space. Finally, heat treatment for thermal fusion process in an oven would be necessary to ensure the plates are fully attached and sealed [12]. Sharifipour et al. [13] studied the effect of clay swelling on the oil recovery factor in a porous medium using micromodels, where the device was made through this process. Furthermore, a laser-etched rock on-chip was also used to resemble the pore space and fracture geometries [14]. Martel et al. [15] utilized the physical properties of fractured bedrocks to design a micromodel etched by hydrofluoric acid on two glass plates. This setup enabled them to understand the critical parameters for an efficient recovery of nonaqueous phase liquids using surfactant solutions. Although the popularity, the conventional glass micromodel manufacturing is a time-consuming and tedious process [16]. Moreover, since non-geological materials are used to build them (e.g., glass, plastic), their properties

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cannot represent most rock samples. In contrast, rock petrophysical properties play an integral role in fluid flow. Among these properties, wettability is one that should be adjusted in such models (e.g., by micromodel aging), enforcing additional steps in preparing the models [17].

To address the above issues, researchers have used natural rocks to fabricate microfluidic pore-network models [18–20]. In a study, a 500-µm rock piece, mounted between two polydimethylsiloxane plates, was used as a microfluidic device [21]. Recently, Teimouri et al. [22] designed and manufactured a transparent cell consisting of two plexiglass plates around a carbonate rock sample to investigate the conformance control during pH-sensitive polymer flooding in a fractured media. The transparent sealing rubber enabled them to photograph the rock surface easily during the experiments. It should be noted that preparing microfluidic models from natural rock samples is challenging since the specimens should be thick enough to avoid chipping during the fabrication, but thin enough to precisely visualize the fluid flow over the entire grooved depth [23, 24]. The main disadvantage of such setups is limitations in their reusability which contradicts the reason for employing such models. This means they can be used solely once for a single run during destructive experiments (e.g., reactive flow), which makes repeating the same experiments impossible.

The micromodel mineral coating approach is receiving increased attention due to providing compositional similarity with natural rocks. For example, Song and Kovscek [25] coated a microfluidic device with clay minerals to mimic a natural rock surface. This method ensured real-time observations of fluid–solid interactions in pore networks. They used this microfluidic model to analyze the effects of brine injection on clay detachments. In a separate study, micromodels were coated with high swelling clay minerals to model the behavior of sandstones that contain swelling clays [13]. Other researchers later used a layer-by-layer self-assembly technique to coat the surface of channels in microfluidic chips with geomaterials [26]. The main challenge of coated micromodels is to make sure a homogeneous layer of coating material with sufficient thickness on the micromodel surface is applied, though they cannot be used in destructive experiments (e.g., acid injection, formation damage).

All of the above fabrication methods try to ensure the resemblance of chemical and physical properties of the inner surfaces to the natural rocks, but they failed to ensure the reusability. Therefore, 3D printing is an alternative technology to build two- or three-dimensional objects from a computer-aided design model by adding materials in layers, which is known as additive manufacturing. Hull [27] developed commercial stereolithography technology for the first time. Additive manufacturing has been applied in different areas of science, including prototyping [28], automotive industry [29], jewelry [30], construction [31], aerospace [32], medicine [33], and petroleum industries [34, 35]. 3D printing is a relatively cheap, rapid, and easy process to analyze fluid flow in porous media [10, 16], which is often faster, cheaper, and less complicated than other microfluidic fabrication methods. Besides, 3D printing technology allows us to alter numerous factors, such as dimension, surface structure and roughness, wettability, and chemical properties of microfluidic domains [36, 37]. The unique feature of this fabrication method is the physical model reproducibility, where several identical copies of the same porous medium can be created which is necessary for destructive experiments.

In several studies, 3D printed core plugs were fabricated to assess the behavior of porous media [38–40]. For example, [41] used gypsum-powder-based 3D printed synthetic samples to study the pore structures (e.g., porosity, pore size distribution, anisotropy) of core plugs. In another study, two 3D printed cylindrical samples with different sizes were fabricated by gypsum powder to investigate the feasibility and reliability of artificial specimens in terms of rock geo-mechanical behavior [42]. Moreover, Kong et al. [43] evaluated the matrix pore structure and alterations after uniaxial compressive strength tests. They examined the overall performance of 3D printing technology in terms of its limitations and flaws. Besides, they tried to study particle and pore structure characterization of 3D printed silica samples using 2D and 3D imaging techniques [44]. A new approach for 3D reconstruction of a rock sample from Computed Tomography (CT) data of a Berea sandstone core plug was proposed, and the resulting 3D image was utilized for printing samples with various printing technologies for comparison purposes [45]. Moreover, the same researchers explained a workflow for creating accurate 3D printed core samples using a machine-learning image processing approach based on the CT data [46]. The pore-scale waterflooding experiments were also carried out on mixed-wetted natural sandstone along with a 3D printed prototype using µCT data [47]. The authors investigated wettability and pore geometry effects on the morphology of the residual oil block. Hasiuk [48] characterized the pore networks using a 3D printed solid porous proxies fabricated by a powder-based 3D printer. Printed rock analogs were manufactured with steel, aluminum, and gypsum powders. The shortcoming of these models is that the saturation distribution as well as fluid pattern through these 3D printed models cannot be investigated visually regardless of the method, (e.g., microscopy) and other advanced techniques (e.g., CT scanning or nuclear magnetic resonance) should be implemented. Thus, there is still a need for microfluidic devices that can be examined visually, which is necessary to better understand the processes that take place during EOR.

Furthermore, 3D printing technology to fabricate simple-shaped micromodels has also been utilized as well, where Watson et al. [16] created a 2D printed micromodel to simulate single-phase flow. Yang et al. [49] fabricated two transparent geometries to study the multiphase flow in a fracture-vug medium using 3D printing technology. They monitored the flow process using the backlight visualization method. The capillary flow and transport phenomena in micron-sized porous media made out of polymer were also investigated using powder-bed fusion printing technology [50]. Ahiiki et al. [51] conducted CO₂ flooding experiments on a multiJet 3D printed fractured porous medium, where simple square pillars were implemented as
fractures within the printed flow cell. One major drawback of these above studies was selecting a very simple pore shape geometry (e.g., lines as fractures) for the microfluidic device that might not be truly representative of a real pore geometry.

In this study, an improved manufacturing method to build microfluidic devices, including complex geometries is developed via 3D printing to investigate multiphase (i.e., miscible and immiscible) pore-scale flow. This complex printed model is derived from CT images of a carbonate rock sample as an input. By implementing image-processing techniques, water breakthrough time, fluid flow path, and the recovery factors are directly determined from the experiments. Moreover, numerical flow modeling is used to evaluate the accuracy of micromodel printing via Structural Similarity Index Measure (SSIM). Collectively, this study offers a novel methodology to analyze fluid flow in a porous medium by fabricating a visual repeatable and reusable microfluidic device. To the best of our knowledge, this is the first time that such an integrated guideline is being introduced for manufacturing 2.5D realistic microfluidic devices (micromodels) from pore-scale rock images where the quality of the printed model is verified by CFD simulations and results can be examined visually. Such a microfluidic device with controlled properties can be used to support our understanding of EOR processes. In other words, this simple model, which is created under controlled conditions, would be a good replacement for destructive laboratory tests and provides a visual tool for examining pore-scale phenomena during EOR processes (e.g., displacement and sweep mechanisms).

2 Methods and materials

2.1 From computed tomography to proxy model

Figure 1 depicts the general workflow in this study. First, CT scanning images [52, 53] were converted to binary series using an image processing procedure via ImageJ, an open-source platform [54] (Fig. 2a). A Region Of Interest (ROI) with a size of $400 \times 400 \times 400$ voxels was selected from printing and further analysis. A non-local mean filter was applied to the CT images to reduce the noise. Then, the K-means clustering-based thresholding algorithm [55] was used for image segmentation (Fig. 2b). The result of this step is a binary image, wherein pores are distinguished from the grains. In the next step, the isolated pores, as well as the pores on the edges of the image (to prevent the fluid leakage), were removed. The image resolution was decreased using the bilinear interpolation method to fit to the resolution of the 3D printer device. Next, an input and an output flow ports were designed in diagonal corners of the microfluidic setup (Fig. 2c). In the final step, the selected image is converted into a 3D model for printing as well as numerical simulations (Fig. 2d). The final dimensions of the printed model is $50 \times 50 \times 5$ mm with a voxel size of $250 \times 250 \times 100$ µm. It is worth mentioning that the resolution decreasing of the original micro-CT image to the 3D printer resolution definitely changes the properties of porous media. To avoid any inconsistency, all further simulations, laboratory experiments, and their related comparisons are performed on the new lower resolution. It should be noted that by 3D printing technology advancement and using printers with higher resolutions, more sophisticated micromodels can be built until an analogue resembling to a natural rock sample with entirely controlled properties can be created. However, the generality of the introduced integrated guideline for manufacturing 2.5D microfluidic devices remains the same.

2.2 Microfluidic model fabrication

To print the microfluidic model, Digital Light Processing (DLP) that uses photopolymers for printing was utilized.
Fig. 2. Illustration of the proxy model preparation. (a) CT scanning image. Select A Region Of Interest (ROI) with a size of $400 \times 400 \times 400$ voxels. (b) Model of (selected ROI) after the image segmentation. (c) Model of (b) after removing the isolated pores and the pores on the edges from the image. A bilinear interpolation method was also performed to increase connectivity. (d) Final 3D image.

Fig. 3. 3D printing procedure. (a) Initial position. (b) The moving arm moves toward the heated resin tank and touches the resin tank bottom (only a small height is left between the build plate and the resin tank bottom). (c) Then the laser beam solidifies the liquid resin captured inside of this height. (d) After the layer consolidating, the moving arm moves upward. (e) The moving arm returns to the initial position, and this process is repeated subsequently to form up the printing object ultimately.
These materials are initially in a liquid state and become harden by using a light source [30]. This printer can fabricate objects layer-by-layer and harden layers by laser beams on the surface of a photo-sensitive liquid resin layer (Fig. 3). The implemented laser (Fig. 3a) is generated by the digital light projector of the 3D printer. The liquid resin is inside of a tank (Fig. 3a) with a transparent bottom so that the projected laser can reach the resin and cure it (Fig. 3c). The build plate (Fig. 3b) simply sticks to the printed object’s surface during printing and moves in the z-direction during the printing process. The build plate’s moving arm descends into the resin and stops at a small height above the bottom of the tank (Fig. 3b). This height is specified by the thickness of the layer that should be printed. In the next stage, the digital light projector illuminates through the bottom of the resin tank (Fig. 3c) only on the model’s particular pixels. This projection cures the resin in those areas into a solid. The cured resin creates the first layer of the proxy model (Fig. 3d), while the remaining uncured pixels are drained from the model. Then, the build platform moves upward to allow for another layer of resin to be cured (Fig. 3e). This process continues until the entire structure of the printing object is fabricated.

A Quantum Queen stereolithography 3D printer (Persia Company) was used to fabricate the proxy model of the rock sample. The resolution in the 3D model was 250 μm in the x and y directions, and the layer thickness was adjusted to 100 μm. Figure 4 depicts the final printed microfluidic media. Table 1 summarizes the 3D printed microfluidic model and the materials specification in detail.

Post-processing plays an essential role in fabricating 3D printed models [38]. It consists of two steps, (1) UV curing and (2) removing the supports and ethanol flushing. UV curing makes the fresh 3D printed microfluidic model to solidify. Because of the Gaussian-shape of the UV light (the UV light intensity decreases at the corners) [56], if the model size is precisely equal to the platform size, the edges will not harden appropriately. Increasing the light intensity to higher values cannot resolve this problem, as the center of the model turns out to be fragile. Therefore, it is suggested that the size of the 3D CAD model be always smaller than the build platform. The model is printed vertically to reduce the adhesion between the printed microfluidic model and the build platform. It also prevents bending and crumbling during the printing process. In our model, several supports were printed with the model in a vertical direction, which must be removed (by the ethanol washing) after printing is accomplished (Fig. 5).

When curing is done, to seal the microfluidic model and avoid fluid escaping from the model during the experiments, two transparent plexiglass sheets (Fig. 6a) were attached to both faces of the printed microfluidic model using screws and bolts (Fig. 6b). It should be mentioned that the screw holes were located in the solid areas of the pore network (i.e., outside of pore space) (Fig. 6c) and did not interference with the pore space. To ensure the model is fully sealed, a PolyDiMethylSiloxane (PDMS) silicone gel was applied on the upper side (solid areas and not pores) of microfluidic device. The plexiglass sheet was then fixed on the upside of the printed model using screws and bolts.

PDMS, also known as dimethylpolysiloxane or dimethicone, belongs to a group of polymeric organosilicon compounds that are commonly referred to as silicones [57]. This silicone gel layer prevents fluid escaping from the area between plexiglass and solid voxels of the printed model and is not in direct contact with pore areas. The transparency of the plexiglass sheets and the 3D printed block...
(i.e., microfluidic model) allows us to access the porous medium for photography purposes easily or cleaning it after each experiment is done (Fig. 6d).

### 2.3 Protocol of experiments

Two scenarios were considered in the experiments, miscible (i.e., tracer test) and immiscible (waterflooding into a saturated microfluidic model with synthetic oil) injection. The synthetic oil in this study is a heptane–toluene, 50–50% solution. The tracer was a very dilute weak Indigo dye \((C_{16}H_{10}N_{2}O_{2})\) solution. Indigo dye is used because of its natural organic nature and with a distinctive blue color [58]. Because of using a very dilute concentration of the dye, its effect on surface tension was ignored. Table 2 summarizes the properties of the fluids. The overall procedure for both laboratory experiments is as follows: (1) the microfluidic model is saturated with the primary fluid, (2) the displacing fluid is injected, (3) a digital camera dynamically captures the flow paths at different time steps, and (4) the captured images are processed for further analyses. Experiments are continued until the displacing fluid front breaks through the outlet port of the microfluidic model.

Table 2. Properties of injected fluids.

| Material name | Company          | Density at 20 °C (kg/m³) | Viscosity at 20 °C Pa s |
|---------------|------------------|--------------------------|------------------------|
| n-heptane     | *MilliporeSigma* | 680                      | 0.0049                 |
| Toluene       | *MilliporeSigma* | 870                      | 0.0043                 |
| Tracer \((C_{10}H_{10}N_{2}O_{2})\) | *Synthesized*  | 998                      | 0.0009                 |

Figure 7 illustrates the schematic of the experimental setup. The microfluidic model is saturated with deionized water and synthesized oil in the miscible and immiscible injection scenarios, respectively. Then, the second fluid is injected through the inlet ports into the printed model with a constant flow rate of 2 ± 0.01 mL/h. To distinguish between the displacing and the displaced fluids, blue dye as a tracer in our experiments were employed. Both miscible and immiscible injection scenarios were repeated twice to verify the results. The injection process is captured by a camera and converted to binary images through image processing techniques. To do so, first, a non-local mean filter is applied to all images to suppress the noise. The images are then converted to black and white (binary) segments by the \(K\)-means Clustering-Based thresholding plugin in the *ImageJ* toolbox.

The contact angle between the synthetic oil and the printed microfluidic model and the plexiglass sheets were measured via the sessile drop technique (Fig. 8). The oil contact angle data for the plexiglass sheets and printed microfluidic models were measured 112° and 122°, respectively. The contact angles of water fluid are 66° and 55° for the plexiglass sheet and printed microfluidic models,
respectively. The result shows that the printed microfluidic model is oil-wet, which makes it superior to the conventional glass micromodels for oil-wet media. Besides, the surface tension result shows that both plexiglass and printed model have very close values. However, the cap sheet of the model can also be 3D printed with the same material of the body.

2.4 Numerical modelling setup

A Computational Fluid Dynamics (CFD) simulator (Ansys Fluent) was employed for the numerical evaluation of the fabricated microfluidic model and to check that the flow paths are not blocked during the printing process. The same structure of the 3D printed tangible model was used for
CFD simulations. Because of the homogeneity in the z-direction, the domain was assumed 2D. The mixture and Volume Of Fluid (VOF) models were used for miscible and immiscible injection processes, respectively. The VOF model can be defined for two or more immiscible liquids. In this model, the fluids share a set of momentum equations for the position of the interface between the fluids. The volume fraction of each fluid is tracked throughout the domain in each computational cell. The mixture and the VOF models differ in three following areas: (i) the inter-phase energy, mass, and momentum transfer are allowed in the mixture model, (ii) the phases can be mixed in the mixture model, and (iii) the mixture model allows the phases to move at different velocities, using the concept of slip velocities [59, 60]. The difference arises between the average velocities of two different fluids flowing together in a flow path. Hence, the slip velocity depends mainly on the difference in the density between the two fluids, and the diffusivity phenomenon. Practically, the diffusion velocity has to be determined by the slip (relative) velocity which is defined as the velocity of dispersed phase relative to the velocity of the continuous phase [61]. Readers can find further details of the mixture and VOF models in the Ansys Fluent user manual [62].

The following parameters were selected based on the fabricated microfluidic model conditions. The flow rate was considered to be equal to 2 mL/h, similar to the experiments. The reference velocity can be calculated from the total cross-section of the input port \( A = 1.56 \times 10^{-3} \text{ m}^2 \) as \( u_{ref} = Q/A = 0.000346 \text{ m/s} \). Moreover, Reynolds numbers were calculated via \( Re = \rho u d/\mu \) for each miscible and immiscible injection scenario as 0.479 and 0.080, respectively. Since both are less than 1, we can be confident that laminar flow regime conditions are satisfied. Since fluid incompressibility was assumed, measuring the absolute pressure value was not necessary; however, the outlet gauge pressure was set to zero. Input and model boundary parameters are summarized in Table 3.

Table 3. Input parameters for the numerical simulations.

| Parameter          | Unit | Miscible simulation | Immiscible simulation |
|--------------------|------|---------------------|-----------------------|
| Outlet pressure \((P)\) | Pa   | 0                   | 0                     |
| Flow rate \((Q)\)   | m\(^3\) s\(^{-1}\) | 5.6e-10             | 5.6e-10               |
| Dynamic viscosity \((\mu)\) | Pa s | 0.0010              | 0.0046                |
| Density \((\rho)\)  | kg m\(^{-3}\) | 982                 | 755                   |

Fig. 9. The 8-bit images of experimental, X, (left side) and numerical, Y, (right side) result. The red boxes are two sample patches \((x, y)\) of 11 \times 11 pixels around a center pixel used for comparing the mean, variance, and covariance of both images. These measure patches are computed for all pixels of the image to find the similarity.

Fig. 10. The velocity profile at the outlet port of the model for mesh independency analysis. The three mesh numbers of 33 280, 101 308, and 320 470 have had the simulation run time of 22, 30, and 73 min, respectively.

Mesh Size Analysis

Velocity vs. Location at Outlet
2.5 Structural Similarity Index Measure (SSIM)

To validate the accuracy of the microfluidic model, we used a direct comparison of the experimental results with the numerical outcome. The images captured during the injection in the microfluidic model were compared with the numerical simulator predictions at the same time steps of the injection phase following the segmentation of the images through Structural Similarity Index Measure (SSIM) [63]. It is worth mentioning that all images have been converted to 8-bit black and white images (Fig. 9). This index has been used in related studies widely [64, 65].

The comparison between the two $X$ and $Y$ images is performed on the basis of these 3 features: luminance ($l$), contrast ($c$), and structure ($s$).

The SSIM compares the luminance, contrast, and structure of two $X$ and $Y$ images locally to quantify the similarity between them. The SSIM index is a decimal value between 0 and 1 where 1 shows a perfect structural similarity, and it happens only when two completely identical images are being compared. A patch of $11 \times 11$ pixels around a center pixel is selected for computing the properties of each center pixel (red boxes in Fig. 9). Hence, the SSIM between two $x$ and $y$ patches of both $X$ and $Y$ images are defined as [66],

$$\text{SSIM} = l(x,y) \times c(x,y) \times s(x,y),$$

where,

$$l(x,y) = \frac{2\mu_x \mu_y + C_1}{\mu_x^2 + \mu_y^2 + C_1},$$

$$c(x,y) = \frac{2\sigma_x \sigma_y + C_2}{\sigma_x^2 + \sigma_y^2 + C_2},$$

$$s(x,y) = \frac{\sigma_{xy} + C_3}{\sigma_x \sigma_y + C_3},$$

therefore;

$$\text{SSIM}(x,y) = \frac{(2\mu_x \mu_y + C_1)(2\sigma_{xy} + C_2)}{(\mu_x^2 + \mu_y^2 + C_1)(\sigma_x^2 + \sigma_y^2 + C_2)},$$

where $\mu_x$ and $\mu_y$ are the average value of $x$ and $y$ patches, respectively, $\sigma_x^2$ and $\sigma_y^2$ are the variance of each $x$ and $y$, and $\sigma_{xy}$ is the covariance of the $x$ and $y$ patches:

$$\mu_x = \frac{1}{N} \sum_{i=1}^{N} x_i, \quad \text{and} \quad \mu_y = \frac{1}{N} \sum_{i=1}^{N} y_i,$$

$$\sigma_x = \left( \frac{1}{N-1} \sum_{i=1}^{N} (x_i - \mu_x)^2 \right)^{\frac{1}{2}}, \quad \text{and}$$

$$\sigma_y = \left( \frac{1}{N-1} \sum_{i=1}^{N} (y_i - \mu_y)^2 \right)^{\frac{1}{2}},$$

$$\sigma_{xy} = \frac{1}{N-1} \left( \sum_{i=1}^{N} (x_i - \mu_x)(y_i - \mu_y) \right).$$

Fig. 11. Different magnification of the computational domain, (a) $1 \times$ magnitude, (b) $4 \times$ magnitude, (c) $8 \times$ magnitude, (d) $16 \times$ magnitude, (e) $32 \times$ magnitude of (a).
$C_1$, $C_2$ and $C_3$ are three constants to ensure stability when the denominator of all fractions becomes 0 and given by,

\begin{align}
C_1 &= (K_1 L)^2, \\
C_2 &= (K_2 L)^2, \\
C_3 &= C_2/2.
\end{align}

$L$ is the dynamic range for pixel values (it was set as 255 since we are dealing with standard 8-bit images). $K_1$ and $K_2$ are just normal constants and equal to 0.01 and 0.03, respectively.

Fig. 12. The captured images of the miscible flow scenario at different time intervals. The left, middle, and right columns show the experiment images, the segmented images of experiments, and numerical simulation results, respectively. (a) Initial condition, (b) 140 s, (c) 340 s, (d) 540 s, and (e) 1300 s (i.e., breakthrough time). The colored areas (pink and blue) represent the injected fluid; the white areas are pores, and the black areas representing solid grains.
3 Results

3.1 Mesh-size

The pore space was populated with a different number of cells (i.e., 33,280, 101,308, and 320,470) to numerically investigate the mesh dependency of the model. Figure 10 illustrates the velocity profile at the outlet port of the microfluidic model with a different number of cells and associated simulation run time on an Intel® Core™ i7, 6700HQ processor. Uncertainty analysis is a systematic study performed to assess the consistency and accuracy of a CFD solver in solving the intended problem. Uncertainty analysis is sub-divided into two processes, verification and validation. Verification assesses the consistency of the solver, whereas, validation evaluates its accuracy. It is expected that the accuracy of results and the simulation run time are increased by raising the number of mesh cells. However, above a mesh number the simulation results remain constant and no changes are observable. The velocity profile prediction of the simulation model with 320,470 mesh does not differ much from the model comprised of 101,308 cells (the velocity variation is less than 4%). Thus, the grid mesh with 101,308 mesh cells was used for further simulations. Figure 11 depicts the final mesh structure of the microfluidic model at different mesh sizes and locations within the microfluidic model.

3.2 Miscible injection scenario

Several images were captured during the entire injection process. Figures 12A–12E depict the distribution of fluids obtained at different time intervals (0, 140, 240, 540, and 1300 s) during the miscible injection scenario. The displaced

| Time (s) | SSIM | Normalized SSIM |
|---------|------|-----------------|
| 0       | 0.95 | 1               |
| 140     | 0.94 | 0.98            |
| 340     | 0.91 | 0.96            |
| 540     | 0.89 | 0.94            |
| 1300    | 0.86 | 0.90            |

Fig. 12. Continued.
and displacing fluids are shown colorless and in blue, respectively. Figures 12F–12J show the binary images of the experimental captured photos analyzed by the ImageJ. It should be mentioned that pink pixels are representing the injected blue-dyed water. Moreover, the prediction of fluid distributions obtained from the numerical simulation of the same microfluidic model is depicted in Figures 12K–12O. As discussed in the previous section, the mixture model was used to simulate this tracer test process (two miscible fluids). Figure 12a shows the microfluidic model at the beginning of an injection test \((t = 0\) s) when it is fully saturated with deionized water. Since the injection process
is miscible, when the colored tracer fluid is injected, both phases would mix. As a result, the injected fluid flowed relatively uniform throughout the entire porous medium, and the breakthrough happened at 1300 s after the start of injection.

Table 4 summarizes the SSIM calculated for the experiments and simulations. The normalized SSIM value of the initial time step is defined as:

\[
\text{Normalized SSIM} = \frac{\text{SSIM}}{\text{SSIM}_{t=0}}.
\]  

Based on Table 4, high similarity values between experimental and numerical results can be observed. Therefore, a good agreement between the results during the miscible injection scenario is obtained. This confirms that the process of fabricating the flow pathways through the introduced 3D printing approach was successful because flow patterns on digital and tangible analogs were similar at the pore scale (Fig. 12).

3.3 Immiscible injection scenario

The entire process of the immiscible injection scenario is repeated just the same as the miscible scenario except before starting the experiment; the microfluidic model was saturated with synthetic oil. To simulate the immiscible injection scenario, the VOF model was used under laminar conditions. The images that are captured during the experiments, the corresponding segmented images, and the numerical predictions are shown in A–E, F–J, and K–O in Figure 13, respectively. The captured images at five different time steps (35, 70, 100, 120, and 133 s) are shown for comparison purposes in this figure.

Comparing the binary images from the experiments with numerical simulation results in Figure 13, it was found that a visual similarity of flow streams in both cases is attained. The SSIM comparing the experiments and simulations is summarized in Table 5. The structural similarity of both experimental and numerical results at the same time intervals was calculated to be above 88%, which reflects a high resemblance between the experimental and numerical results (normalized SSIM > 0.95) during the immiscible injection scenario. This similarity again represents that implementing our printed technology to fabricate the microfluidic model was reliable, and the printed model at the pore-scale has similar behavior to the rock analog that was based on the CT data of a natural specimen.

Figure 13 explains that during the immiscible flooding scenario, oil production took place mostly before the breakthrough time (133 s). After the breakthrough happens, the
of the results. The idea was to manufacture a reproducible transparent microfluidic model directly from actual rock. A comprehensive guideline was presented to verify the quality of the printed microfluidic model using parallel CFD simulation of true flooding processes on the printed model images. This microfluidic model was subjected to single and multiphase injection scenarios. Furthermore, the same processes were simulated by a CFD numerical simulator to ensure the flow paths are not blocked during the printing process. Flow stream comparison of the segmented experimental images with the numerical simulation predictions in both miscible and immiscible scenarios indicated high similarities in our relatively complex pore geometry. The obtained results from the CFD simulations and the experimental data were compared in 2D by a similarity measure index, known as SSIM. The normalized measured index showed an acceptable similarity of both miscible (>90%) and immiscible (>95%) injection scenarios. Thus, it can be concluded that fabricating the microfluidic model by the DLP 3D printing technology from the CT-images of the natural rock samples looks promising, and this technology can be an appropriate tool for reproducing microfluidic porous media in the future. Reproducing reusable porous media with known properties has a variety of applications in the petroleum industry, especially in analyzing reactive flow in porous media. The authors acknowledge that the current printing technology still has limitations in terms of resolution, overall device dimensions, and resin versatility for pore-scale flow analysis. However, the introduced guideline for printing 2.5D micromodels can provide potential for fluid flow studies.

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**Table 5.** The SSIM index between the immiscible scenario images of the experiments and simulations at different time intervals.

| Time (s) | SSIM  | Normalized SSIM |
|---------|-------|-----------------|
| 35      | 0.92  | 0.99            |
| 70      | 0.92  | 0.98            |
| 100     | 0.91  | 0.97            |
| 120     | 0.89  | 0.95            |
| 133     | 0.89  | 0.95            |

**Fig. 14.** The oil recovery factor of the immiscible injection scenario.

displacing fluid only will flow through the same path within the pore space and exit the microfluidic model without any further oil displacement on new routes. The recovery factor at various time steps of the experiments was calculated by measuring the number of colored pixels of the displacing fluid divided by the total area of the microfluidic model that is filled with the displaced fluid. Results exhibit that the recovery factor increased until the breakthrough time is achieved, and then stayed stagnant. To ensure the accuracy of the experiments, the process was repeated twice (setup was cleaned entirely before the second round), and results are compared with the predictions of the VOF model, shown in Figure 14. The final recovery factor was 40 ± 3%, while an excellent agreement between VOF with both rounds of the experiments is achieved.

As the results show, unlike the previous studies [9, 16, 49], a more complex geometry – adopted from rock CT scanned images – has been used in this study. The fabrication materials was oil-wet initially as opposed to the conventional glass micromodels that need additional steps for wettability alteration of models [10, 11]. Furthermore, if the setup is used in destructive experiments [23, 24], repeatability of experiments on reproducible microfluidic devices is the main motive of using such 3D printed models.

**4 Conclusion**

This study investigated the pore-scale flow through a heterogeneous carbonate rock using the digital-light processing 3D printing technology through direct observation
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