Monochromatic multicomponent fluorescence sedimentation velocity for the study of high-affinity protein interactions

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Abstract The dynamic assembly of multi-protein complexes underlies fundamental processes in cell biology. A mechanistic understanding of assemblies requires accurate measurement of their stoichiometry, affinity and cooperativity, and frequently consideration of multiple co-existing complexes. Sedimentation velocity analytical ultracentrifugation equipped with fluorescence detection (FDS-SV) allows the characterization of protein complexes free in solution with high size resolution, at concentrations in the nanomolar and picomolar range. Here, we extend the capabilities of FDS-SV with a single excitation wavelength from single-component to multi-component detection using photoswitchable fluorescent proteins (psFPs). We exploit their characteristic quantum yield of photo-switching to imprint spatio-temporal modulations onto the sedimentation signal that reveal different psFP-tagged protein components in the mixture. This novel approach facilitates studies of heterogeneous multi-protein complexes at orders of magnitude lower concentrations and for higher-affinity systems than previously possible. Using this technique we studied high-affinity interactions between the amino-terminal domains of GluA2 and GluA3 AMPA receptors.

Introduction The dynamic formation of multi-protein complexes is a key step in the assembly of supramolecular structures and in the regulation of many cellular processes (Wu, 2013; Li et al., 2012; Gavin et al., 2002; Krogan et al., 2006; Wu and Fuxreiter, 2016). For example, in immunological signal transduction the assembly of adaptor protein complexes into micro-clusters after T-cell activation plays a critical role in the sensitivity and specificity of activation (Sherman et al., 2011; Dustin and Groves, 2012). Another well-known multi-protein complex is the post-synaptic density, a large structure assembled via interactions between many different scaffolding proteins, signaling proteins and ligand gated ion channels, that regulates postsynaptic neurotransmission and plasticity (Kennedy, 2000; Ferré et al., 2007; Kumar and Mayer, 2012). Many of the protein interactions involved in the assembly of such molecular machinery are multivalent (Li et al., 2012; Houtman et al., 2006;
Coussens et al., 2013). This often allows structurally polymorph complexes to co-exist (Wu and Fux-reiter, 2016), posing formidable challenges for any biophysical method to elucidate basic architectural principles and driving forces, which requires the study of reversible interactions of multiple protein components with multiple states.

Sedimentation velocity analytical ultracentrifugation (SV) is a classical technique that allows determination of the number, size, and shape of reversibly formed protein complexes, and provides information on their affinity, stoichiometry and binding kinetics (Schuck, 2013, 2015). Though a long established technique, it is worth recapitulating the basic principles of SV (Figure 1). In SV the spatio-temporal evolution of macromolecular concentration profiles in a sample solution after application of a strong centrifugal field is optically monitored in real-time. SV has unique opportunities for studying protein interactions, since—different from separation techniques—faster sedimenting protein complexes will always remain in a bath of slower-sedimenting constituent components, such that the association/dissociation of non-covalent complexes is maintained throughout the experiment (Figure 1). Since sedimentation takes place free in solution, the analysis can be based on first principles and mathematical models for the sedimentation/diffusion process, and modern size-distribution analysis results in sedimentation coefficient distributions with high hydrodynamic resolution. Thus, SV has emerged as a powerful technique in the study of the solution state behavior of complex interacting systems of macromolecules, including ion-channels, adaptor proteins, membrane proteins, nucleic acids, and carbohydrates (Kumar and Mayer, 2012; Houtman et al., 2005; le Maire et al., 2008 Niewiarowski et al., 2010; Padrick and Brautigam, 2011; Harding et al., 2015; Jose et al., 2012). Extended to multi-signal analysis SV can distinguish different sedimenting
components from characteristic extinction properties, directly revealing binding stoichiometries and resolving co-existing complexes (Houtman et al., 2006; Coussens et al., 2013; Padrick and Brautigan, 2011; Balbo et al., 2005; Barda-Saad et al., 2010). For example, through applications of this approach an essential mechanism for the formation of signaling particles in T-cell activation (Houtman et al., 2006; Coussens et al., 2013; Barda-Saad et al., 2010) was discovered to be the multivalent intracellular oligomerization of LAT via three-component adaptor protein complexes (Houtman et al., 2006). Such biophysical multi-protein solution studies naturally complement super-resolution fluorescence imaging and co-localization studies of live cells (Sherman et al., 2011; Houtman et al., 2006; Coussens et al., 2013; Barda-Saad et al., 2010). But, unfortunately, traditional SV is limited in several ways by optical detection systems that generally require the use of micromolar concentrations of purified proteins.

Recently, analytical ultracentrifugation was enhanced by the availability of a commercial fluorescence optical detection system (FDS), that uses confocal detection radially scanning the sample in the spinning rotor (MacGregor et al., 2004) (Figure 2a). After accounting for characteristic data features, the FDS allows highly quantitative analyses of the sedimentation process (Zhao et al., 2013b),
extending the sensitivity of SV by several orders of magnitude into the low picomolar range (Zhao et al., 2014a; Le Roy et al., 2015). This enables the measurement of binding energies in self-and hetero-association with very high affinity (Zhao et al., 2012; 2013a; 2014a), and also makes it possible to study proteins that are relatively scarce, not well purified, and in some cases even in cell extracts (Le Roy et al., 2015; Polling et al., 2013; Kingsbury and Laue, 2011; Kokona et al., 2015). Unfortunately, these advantages come with a drawback of having only a single excitation wavelength, either 488 nm or 561 nm, due to the technical constraints of accommodating a moveable confocal optical system inside the evacuated rotor chamber of the ultracentrifuge. Thus, spectral discrimination of multiple components is not available in AUC fluorescence detection, which significantly limits the study of multi-protein complexes.

In the present work, we embark on a different approach for multi-component analysis based on photophysical properties of photoswitchable fluorescent proteins (psFPs). The psFPs make up a class of fluorescent proteins that can be actively switched between fluorescent and non-fluorescent states using different wavelengths of illumination. While they have been engineered for entirely different purposes in nanoscience and fluorescence imaging, we have previously observed that under the illumination conditions of FDS-SV they are induced to slowly switch by virtue of the excitation light.
when radially scanning the spinning sample (Zhao et al., 2014b). Even though the mechanism of photoswitching in psFPs generally may involve multiple states, in the low-power exposure that occurs during sedimentation using the FDS the process is quantitatively modeled very well as a single exponential. This is exploited and further developed in the present work. Different classes of psFPs exhibit different time-courses of photoswitching in FDS-SV, and may be switched on to a fluorescent state or switched off to a dark state. We show that this process is highly quantitative, and how this signal change can be manipulated spatially and temporally during sedimentation. The new spatio-temporal signal dimension is folded into the computational analysis of the sedimentation process, and thus offers an avenue for monochromatic multi-component (MCMC) detection. Using existing commercial FDS instrumentation, the MCMC approach allows us to simultaneously determine separate sedimentation coefficient distributions for each class of fluorophore, which can be used to determine the identity and binding stoichiometry of hydrodynamically resolved complexes of psFP-tagged proteins.

We first demonstrate experimental proof of principle of exploiting the photo-switching kinetics as a novel aspect of fluorophore analysis. Using psFPs commonly employed in super-resolution microscopy, we show an example for the identification of binding partners in a three-component protein mixture. We then use this approach to study the high-affinity interactions of glutamate receptor GluA2 and GluA3 amino terminal domains, which engage in competitive homo-dimerization and hetero-dimerization processes that are thought to control the combination of receptor subtypes into diverse homomeric and heteromeric ion channel tetramers with different gating properties (Kumar and Mayer, 2012; Rossmann et al., 2011; Herguedas et al., 2016).

Results

Fluorescence signals of psFPs in sedimentation velocity

Fluorescence SV signals of psFPs are highly unusual when compared to the temporal evolution of concentration profiles in traditional AUC (Figure 2b), in that they exhibit sedimentation boundaries modulated by characteristic signal magnification or diminution on the time-scale of sedimentation (Figure 2c,d). This is caused by the 488 nm excitation beam of the FDS scanner which induces photoswitching between fluorescent and dark states. But in contrast to typical power densities of \( \sim \text{kW/cm}^2 \) for photoswitching on the millisecond time-scale (Grotjohann et al., 2012), the transient exposure in FDS-SV during radial scanning and sample rotation leads to a time-averaged incident power density that is \( \sim 10^5 \)-fold weaker. This slows the photoswitching kinetics down to the time-scale of...
hours, commensurate with the sedimentation process in SV. A prerequisite for exploiting this new temporal dimension for the multi-component decomposition of fluorescence SV data is the ability to precisely describe the signal evolution of the individual psFPs. We have developed a model Equation 4 that assumes a single-step process with constant quantum efficiency for switching, while accounting for the radially non-uniform exposure during scanning (caused by psFPs transitioning through the beam in a shorter time as they migrate to higher radii at the same angular velocity). Combined with a description of molecular sedimentation and diffusion, the model predicts signal boundaries to be subject to an exponential overall signal modulation with slightly radially sloping solution plateaus, with a small positive slope for those switching off (Figure 2c) and a small negative slope for FPs switching on (Figure 2d) under 488 nm illumination. As shown in the examples of Figure 2, fits of this model to within the noise of data acquisition can routinely be achieved for the fluorescence sedimentation data of diverse FPs, including, for example, the rapidly de-activating rsEGFP (Grotjohann et al., 2012) and the strongly activating Padron (Andresen et al., 2008) (Figure 2c,d). From the fits of the single component samples, we can obtain the relative amplitude and time-constant of photoswitching for different fluorophores, which serves as a highly reproducible, characteristic temporal tag. For example, for rsEGFP with a scanning beam of 13 mW we measure a depletion rate of 5.08 [4.97–5.19; 95% CI]/sec, approaching a final fluorescence of 13.4 [13.0–13.9; 95% CI]% its initial value, associated with a particle sedimentation coefficient of 2.50 [2.45–2.54; 95% CI] S and apparent molar mass of 29.5 [26.5–33.0; 95% CI] kDa. By contrast, as previously established (Zhao et al., 2014b), no photophysical processes are detectable under this illumination for other fluorophores such as fluorescein-based DL488 (Figure 2b) and standard EGFP.

**MCMC decomposition of mixtures**

The strikingly different signal patterns in sedimentation of psFPs can be utilized for the computational decomposition of sedimentation data of mixtures into separate sedimentation coefficient distributions for each differently tagged component. As an initial proof of principle, Figure 3a shows sedimentation data of a mixture of rsEGFP2 and FITC-BSA. The shape of the signal boundaries is governed jointly by the signal time-domain, polydispersity in the sedimentation coefficient distribution, as well as diffusion. The initially strongly decreasing plateau intensity over time is a characteristic of rsEGFP2 signals that can be readily visually discerned and distinguished from the stable fluorescein signal that causes the plateaus to stabilize at approximately half the total loading signal. In addition to the decreasing plateau, the decreasing amplitude of the sedimentation boundary also carries significant information on the time-dependent rsEGFP2 signal. This is highlighted in Figure 3b by the failure of an impostor fit with conventional boundary analysis, in which the decreasing plateau level are compensated for with ad hoc inclusion of time-dependent baseline offsets (usually absent in FDS-SV [Schuck et al., 2015; Zhao et al., 2013b]).

In the MCMC analysis the fluorophore photoswitching parameters were fixed to predetermined values of the individual fluorophores (run side-by-side in a different rotor position). The
Figure 3. Mono-chromatic multi-component (MCMC) decomposition of mixtures. (a) Evolution of radial fluorescence profiles of 20 nM rsEGFP2 and 30 nM FITC-BSA sedimenting at 50,000 rpm and 20°C. Raw data are shown as points with higher color temperature indicating the passage of time (only every second scan shown), and solid lines are the best-fit based on the MCMC distribution model with two components, producing residuals as shown in the lower panel attached. (b) An impostor fit with a conventional c(s) analysis not accounting for time-dependent signal increments, but compensating their effect on plateau levels by artificial inclusion of time-dependent baseline offsets, creates large misfit in the boundary region. (c) The resulting sedimentation coefficient distributions of each fluorophore component from the MCMC analysis of the mixture (solid lines) and in separate control experiments with individual samples (dashed lines). (d) Fluorescence sedimentation data acquired under the same conditions for a mixture of 20 nM rsEGFP2, 20 nM Padron, and 50 nM anti-GFP mAb, presented in the same format as (a). (e) Analogous to (b), showing the best-fit ‘conventional’ boundary model not accounting for time-dependent signal increments while including artificial baseline parameters. (f) Resulting sedimentation coefficient distributions from the MCMC analysis (solid lines) and standard control experiments (dashed lines).

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The following figure supplement is available for figure 3:

Figure supplement 1. Sedimentation signals of rsEGFP2-GluA3.
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MCMC decomposition via Equation 5 results in an excellent fit (Figure 3a), with sedimentation coefficient distributions of species with temporal signal characteristics of fluorescein and rsEGFP2 as shown in Figure 3c (solid lines). The decaying component is correctly found to migrate with ~2.5 S, and the temporally stable signal is found to sediment in the usual hydrodynamically resolved monomer, dimer, and trimer peaks of BSA. The relative errors in the distinction between rsEGFP2 and fluorescein components are calculated to be 0.21% over the entire range (based on Equation 6).
The sedimentation coefficients extracted from the mixture are highly consistent with those obtained in control experiments of individual protein components (dashed lines in Figure 3c), as expected for a mixture of non-interacting species.

Fluorescence SV data from a three-protein mixture with interactions is shown in Figure 3d, consisting of two psFPs (rsEGFP2 and Padron), in addition to a molar excess of unlabeled monoclonal anti-GFP antibody (mAb). From visual inspection of the data one can discern a boundary structure with more complex temporal modulation, which, again, cannot be accounted for with any conventional boundary model (Figure 3e). Application of the MCMC decomposition produces an excellent fit, with component sedimentation coefficient distributions (Figure 3f solid lines) again being highly consistent with the results from the separately measured Padron and rsEGFP2/mAb mixture (Figure 3f dashed lines). Here, the sedimentation coefficient distribution of rsEGFP2 shows a 7 S peak with no 2.5 S peak, consistent with the formation of an antibody/rsEGFP2 complex. Thus, the binding partner of the antibody can be correctly identified by exploiting the new temporal signature dimension characteristic of the psFPs. Based on Equation 6, the relative error in assignment of component concentrations is 2.6% at 2.5 S and 1.1% at 7 S. Thus, these model systems demonstrate the potential for simultaneous component discrimination and hydrodynamic resolution.

**Choice of psFPs, switching kinetics and laser power**

When the psFPs are involved in complex formation, the question arises whether the photoswitching kinetics of psFPs may also depend on the complex state. In fact, in modeling the data of Figure 3d, the time-constants of rsEGFP2 were initially constrained to the separately measured values, but subsequent refinement led to a significantly better fit: As may already be visually discerned from comparison with Figure 3—figure supplement 1, a portion of the fast-moving boundary of the rsEGFP2/mAb complex in Figure 3d remains fluorescent after long time ($\alpha = 0.2070 \ [0.2052–0.2088$, 95% CI$]$), whereas free rsEGFP2 shows nearly complete conversion to the dark state ($\alpha = 0.0274 \ [0.0270–0.0281$, 95% CI$]$). Clearly, when bound by the anti-GFP antibody, the contrast of rsEGFP2 is lower than in the unbound state. Similar observations were made with rsEGFP, which exhibits slightly altered photoswitching kinetics in the presence of the anti-GFP antibody (data not shown). These observations were confirmed by rsEGFP and rsEGFP2 fluorescence measurements in a benchtop fluorimeter (Figure 4a), where we found marked alterations in the off rates and on/off contrast ratios for both rsEGFP and rsEGFP2 in the presence of antibody as compared to their unbound state. At the same time, their emission spectral properties changed little with the addition of the antibody (Figure 4b). These effects point to possible conformational changes induced by antibody binding impacting the equilibrium of photophysical states (see Discussion). In general, however, such effects should be irrelevant in applications of this approach where the psFP will be designed as an inert tag rather than offering a binding site.

We have found that several psFPs are suitable for FDS-SV with well-defined photophysical characteristics under the current illumination conditions. Besides rsEGFP, rsEGFP2 and Padron these also include Dronpa (Zhao et al., 2014b). While older FDS instruments are equipped with a fixed-power 13 mW solid-state laser, newer models operate with an adjustable 50 mW diode laser that offers additional flexibility for modulating photoswitching kinetics by using different power settings for the scanning beam. The optimal choice of psFP and excitation power will be determined by consideration of the temporal conversion characteristics of all psFPs in the mixture, in combination with the expected time-course of sedimentation, as dictated by $s$-value of the protein complex and the rotor speed. We have implemented Equation 6 in the data analysis software as a design tool that – prior to data acquisition – can guide the psFP selection to maximize the contrast for MCMC based on known psFP characteristics in FDS and the sedimentation coefficient range of the expected protein complexes. For example, the black line in Figure 5 shows the theoretically best switching rate constant for a 2.8 S species under standard SV conditions to be between 1–5 $\times$ 10$^{-4}$/sec.

**Blinking and FRAP-like sedimentation with psFPs**

It is evident that switching of psFPs is required for discrimination, but at the same time the decaying boundary amplitudes for psFPs that switch off during sedimentation will diminish the information content on such psFPs-tagged species, as the signal disappears at later times. However, rapid photoswitching can be advantageous if we exploit the reversibility of the process to switch it back on.
Stopping the 488 nm exposure will cause rsEGFP to spontaneously relax back into the equilibrium fluorescent state on the time-scale of an hour. Thus, passive restoration of the fluorescent signal by simply pausing the data acquisition is possible (data not shown) but presents a viable approach only for slowly sedimenting species. However, rapid and virtually complete restoration of the initial psFPs signal is possible by illumination at 405 nm. In this way, for example, rsEGFP and rsEGFP2 can undergo hundreds of on/off cycles with very little loss (Grotjohann et al., 2012). To this end, we took advantage of the window in the rotor chamber that usually forms part of the interference optical system, and modified it to allow illumination of the spinning rotor with a high-power 405 nm LED at ~10 mW/cm². To achieve a quantitatively uniform reset of fluorescence, a sector-shaped mask was used to produce constant 405 nm exposure times for molecules rotating through the beam at all radii. SV experiments were carried out with several cycles of rapid signal depletion under 488 nm illumination at 25 mW (producing a depletion rate of $9.7 \times 10^{-4}$/s for rsEGFP2), alternating with a 2 min pulse of 405 nm illumination (leading to > 98% recovery of the fluorescence signal of rsEGFP2). The sequence of exposure and scanning events is schematically represented in Figure 6a. An example for the resulting ‘blinking’ boundary for rsEGFP2 is shown in the Video 4 and Figure 6b. An experiment with Padron exhibiting the opposite blinking behavior is shown in Figure 6b. With signal recovery time-points included into the model, blinking SV data could be fitted within the noise of data acquisition, and blinking has been fully implemented in the MCMC decomposition of signals from mixtures with different fluorophores. However, on the basis of the theoretical analysis of information content in Figure 5 (magenta line), for switching processes at rates below $3 \times 10^{-4}$/sec, blinking can be detrimental to component discrimination, because it does not allow the fluorophore to ever significantly populate the dark state.

Figure 5. Calculated relative concentration error for distinguishing photoswitching from non-switching FPs in SV, with and without blinking. The calculations are based on a decaying signal contribution of the psFP with different rate constants, assuming standard sedimentation conditions (12 mm solution column, 20°C, 50,000 rpm, similar to data shown in Figure 2c) and an s-value of 2.8 S. Shown are the predictions of Equation 6 for constant scanning (black) and blinking (magenta) with 2 min reset events occurring at 26 min and 69 min.

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Stopping the 488 nm exposure will cause rsEGFP to spontaneously relax back into the equilibrium fluorescent state on the time-scale of an hour. Thus, passive restoration of the fluorescent signal by simply pausing the data acquisition is possible (data not shown) but presents a viable approach only for slowly sedimenting species. However, rapid and virtually complete restoration of the initial psFPs signal is possible by illumination at 405 nm. In this way, for example, rsEGFP and rsEGFP2 can undergo hundreds of on/off cycles with very little loss (Grotjohann et al., 2012). To this end, we took advantage of the window in the rotor chamber that usually forms part of the interference optical system, and modified it to allow illumination of the spinning rotor with a high-power 405 nm LED at ~10 mW/cm². To achieve a quantitatively uniform reset of fluorescence, a sector-shaped mask was used to produce constant 405 nm exposure times for molecules rotating through the beam at all radii. SV experiments were carried out with several cycles of rapid signal depletion under 488 nm illumination at 25 mW (producing a depletion rate of $9.7 \times 10^{-4}$/s for rsEGFP2), alternating with a 2 min pulse of 405 nm illumination (leading to > 98% recovery of the fluorescence signal of rsEGFP2). The sequence of exposure and scanning events is schematically represented in Figure 6a. An example for the resulting ‘blinking’ boundary for rsEGFP2 is shown in the Video 4 and Figure 2e. An experiment with Padron exhibiting the opposite blinking behavior is shown in Figure 6b. With signal recovery time-points included into the model, blinking SV data could be fitted within the noise of data acquisition, and blinking has been fully implemented in the MCMC decomposition of signals from mixtures with different fluorophores. However, on the basis of the theoretical analysis of information content in Figure 5 (magenta line), for switching processes at rates below $3 \times 10^{-4}$/sec, blinking can be detrimental to component discrimination, because it does not allow the fluorophore to ever significantly populate the dark state.

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Figure 6. Blinking fluorescence SV data. (a) Cartoon illustrating the timing of events in standard vs. blinking experiments. Dependent on sample history, an initial brief illumination with 405 nm may be applied prior to start of centrifugation. In standard time-domain experiments (top) a series of 488 nm scans at constant frequency is initiated shortly after full rotor speed is reached. It causes a gradual depletion of signals for molecules switching off, depicted by the fading blue bar, such as shown in Figure 2c. For blinking experiments (middle and bottom) the sequence of scans was briefly interrupted at select time points (indicated by purple arrows) by short pulses of high-power 405 nm illumination, switching on molecules that switch off at 488 nm such as rsEGFP2 in Figure 2e, or switching off molecules that switch on at 488 nm such as Padron in (b), respectively. (b) Example of blinking data from 30 nM Padron sedimenting at 50,000 rpm and 20°C. Fluorescence scans were acquired with 488 nm excitation in ~5 min intervals (only every second scan shown), interrupted three times by 2 min exposure of the spinning rotor to 405 nm light. During the data acquisition cycles the fluorescence signal increases, due to
For the slow switching case, we followed a different approach to enhance discrimination by creating a spatially localized trough in the psFP fluorescence signal. In contrast to blinking, this can be executed without any instrument modification, simply by positioning the existing FDS detector at a fixed radius for an extended period of time at the beginning of the sedimentation process. Based on the size of the focal spot we estimate the stationary exposure to be on the order of 100-fold stronger as compared to the time-averaged exposure during scanning across the standard radial scan range. Localized switching to the dark state causes a trough in the fluorescence signal (or a peak for molecules switching on at 488 nm). Much like the well-known technique of fluorescence recovery after photobleaching (FRAP), molecules in the dark state that are located initially in the trough will diffuse and exchange with fluorescent molecules from outside, diminishing the trough. In contrast to FRAP, the diffusion processes are coupled to size-dependent migration from sedimentation, which translates and stretches the shape of the trough as it diminishes. Simultaneously, this process is superimposed by the same uniform photoswitching of psFPs that sets in with radial scanning (Video 5). Even though this appears to be a more complicated process, the evolution of the trough is naturally modeled in the same framework developed above for the sedimentation in quasi-uniform exposure: Since SV models already account for diffusional spread superimposed to sedimentation, the FRAP-like SV model solely requires the additional application of appropriate boundary conditions (Equation 8) at early times. However, in comparison to standard sedimentation boundaries, the resulting data are enriched in several ways, as (1) additional information on diffusion becomes available; (2) two additional sedimentation boundaries are generated to improve the precision of

![Diagram](image)

**Figure 7.** Cartoon of the mixed homo- and hetero-dimerization of GluA2-ATD and GluA3-ATD. DL488-GluA2 (magenta) exhibits moderately strong homo-dimerization, while rsEGFP2-GluA3 (blue) undergoes weak homo-dimerization. Both are competitive with a strong hetero-association. DL488-GluA2 provides a constant fluorescent signal contribution, whereas rsEGFP2-GluA3 signals are modulated and can be recognized in the time-domain of the signal.

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Figure 8. Analysis of the self-association of DL488-GluA2 and rsEGFP2-GluA3. (a) DL488-GluA2 samples at a series of concentrations from 0.2 nM to 200 nM were sedimented at 50,000 rpm, 20°C and FDS scans were acquired with 488 nm excitation. The resulting SV data were fit to a c(s) model. (b) Isotherm of s_w-values determined by integration of c(s) profiles in (a) (circles). The monomer-dimer model of the isotherm (solid line) leads to best-fit values of s_1 = 3.57 S, s_2 = 5.11 S (uncorrected s-values) and a best-fit K_{d,22} of 24 [9–59; 95% CI] nM. (c) Sedimentation coefficient distributions of rsEGFP2-GluA3 at concentrations between 1 nM and 30 nM, determined Figure 8 continued on next page.
sedimentation coefficients; and (3) in data from mixtures of psFPs with stable fluorescent molecules, the depth of the trough will provide a landmark at early times reporting directly on the concentration of psFPs-tagged components. In applications to the analysis of experimental data, excellent fits were achieved with this model with residuals close to the noise of data acquisition. For example,

Figure 8 continued

in blinking configuration as shown in Figure 2e. The constant peak in this concentration range is consistent with the previously determined $K_{d,33}$ of 5.6 μM (Zhao et al., 2012).

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Figure 9. Competitive self-association and hetero-association of DL488-GluA2 and rsEGFP2-GluA3. Scan data were acquired by FDS-SV, continuously scanning with 488 nm excitation during the sedimentation at 50,000 rpm, 20°C. Data shown are for equimolar concentrations at 0.3 nM (a), 3 nM (b) and 10 nM (c). Solid lines and residuals are from the MCMC decomposition, with pre-determined switching parameters for rsEGFP2-GluA3, leading to distributions shown in Figure 10a.

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with the single-species model fitted to the rsEGFP2-GluA3 data shown in Figure 2f, the $s$-value is 4.59 [4.50–4.68, 68% CI] S, consistent with the value obtained from blinking and from constant illumination experiments.

**Application to the GluA2 – GluA3 ATD interaction**

Glutamate receptor ion channels (iGluRs) assemble into homo- and hetero-tetramers with their subtype composition dictating the properties of synaptic transmission (Geiger et al., 1995). It is thought that the strength of homo- and hetero-dimerization of the amino-terminal domains of different iGluRs governs their assembly and tetrameric architecture (Rossmann et al., 2011; Kumar et al., 2011). Therefore, the binding affinities of iGluRs have been of significant interest (Zhao et al., 2012; Rossmann et al., 2011; Karakas et al., 2011; Clayton et al., 2009; Kumar et al., 2009). In a pioneering study, homo- and hetero-dimerization affinities for different AMPA receptor amino terminal domains (ATDs) were determined by standard FDS-SV (Rossmann et al., 2011). However, for analysis of hetero-oligomerization only one component could be monitored, and the FAM-label used in that study was later found to induce artificially strong homo-dimerization of GluA2 ATD (Zhao et al., 2013c), with its effect on interactions with the other AMPA receptor subunit ATDs unknown. Recent work, which has resulted in structures of full length heteromeric AMPA receptors assembled from GluA2 and GluA3 (Herguedas et al., 2016) provides a compelling reason for accurately measuring the affinity for assembly of GluA2/GluA3 ATD heterodimers. Using Dylight488-labeled GluA2-ATD (DL488-GluA2) and a fusion protein of GluA3-ATD and rsEGFP2 (rsEGFP2-GluA3), we take advantage of the component discrimination in MCMC to monitor simultaneously the homomeric and heteromeric complexes, which consist of GluA2 monomers and homodimers, GluA3 monomers and homodimers, and GluA2/GluA3 heterodimers (Figure 7). In the initial control experiments, a dilution series of DL488-GluA2 (Figure 8a,b) yielded a homo-dimerization $K_{d,22}$ of 24 [9–59; 95%CI] nM; no homo-dimerization was detected for rsEGFP2-GluA3 at concentrations up to 30 nM (Figure 8c). These results are consistent with previously measured $K_{d,22}$ and $K_{d,33}$-values for the homo-dimerization of GluA2 and GluA3, 20.5 nM [15.9–26.4; 95% CI] (Zhao et al., 2013a) and 5.6 [1.7–14] µM (Zhao et al., 2012), respectively, while by contrast, the homo-dimerization $K_{d,22}$ of 1.8 nM for FAM-labeled GluA2 was 11-fold lower (Rossmann et al., 2011).

To analyze the heterogeneous interaction between GluA2 and GluA3 ATDs, an equimolar dilution series from 0.1–30 nM was studied in a configuration with a 13 mW excitation beam, distinguishing rsEGFP2-GluA3 from DL488-GluA2 solely from slow photoswitching of the former. Representative raw
data sets and MCMC fits to the sedimentation boundaries are shown in Figure 9, leading to calculated component sedimentation coefficient distributions shown in Figure 10a. At a high concentration of 30 nM, the sedimentation coefficient distributions rsEGFP2-GluA3 and DL488-GluA2 both show a single co-sedimenting peak at ~5.9 S, consistent with a saturated 1:1 hetero-dimer complex, moderately extended with a frictional ratio of 1.42. With decreasing concentrations the peaks occur at lower sedimentation coefficients, characteristic for a rapid association/dissociation equilibrium relative to the
time-scale of sedimentation (Schuck, 2010). Due to the decreasing signal/noise ratio peaks also broaden at lower concentrations. Further, at concentrations below 1 nM a separate slower sedimenting peak of DL488-GluA2 can be discerned, consistent with the s-value of free GluA2 monomer, co-existing with a faster-sedimenting dimeric fraction of GluA2. Due to the smaller difference between the s-value of the hetero-dimeric complex and free rsEGFP2-GluA3, the latter cannot be resolved at the low signal/noise ratios below 1 nM. However, the signal-weighted average sedimentation coefficient $s_w$ can still be determined as a function of concentration for both components (Figure 10b). The Monte-Carlo error analysis shows $s_w$ to be well-defined at all concentrations for the constant signal component, but for the decaying signal component statistical errors increase at lower concentrations, with the lowest useful data point at 0.3 nM. A global fit with an isotherm model for the coupled system where hetero-oligomerization of GluA3 is competitive with homo-oligomerization of GluA2 leads to an estimate of the heteromer $K_{d,23}$ of 0.32 [0.20–0.46, 95% CI] nM.

To explore an alternative MCMC design, an experiment with the FRAP-like SV configuration was carried out (Figure 11). Mixtures of rsEGFP2-GluA3 and DL488-GluA2 were exposed to localized 488 nm light from the stationary FDS for a period of 20 min. The initial illumination was assessed from the analysis of a control psFP sample spinning side-by-side in the same rotor sharing the same exposure (Figure 2f), and then fixed for the analysis of the mixtures (Figure 11). Visually, the reduced trough depth directly reflects the smaller relative signal contribution of rsEGFP2. Consistent with the results from the previous experimental series, the weight average component sedimentation coefficients series from the FRAP-like SV leads to an estimate of the heteromer $K_{d,23}$ of 0.68 [0.36–1.24, 95% CI] nM (Figure 12).

**Discussion**

The present work shows the proof of principle for how different macromolecular components can be readily distinguished in fluorescence-based sedimentation velocity experiments using single wavelength excitation in a way that is naturally compatible with many fluorescent probes commonly used in super-resolution microscopy. Although psFPs were designed to serve a very different purpose, we
have embarked on the quantitative analysis of their switching kinetics as a novel temporal tag to substitute for spectral discrimination. In the low-power illumination conditions of FDS-SV the time-course of photoswitching can serve as a finger-print for different psFPs and permit quantitative multi-component analysis. Thus, the study of heterogeneous interactions can be carried out with mixtures of psFP-tagged proteins, proteins labeled with stable fluorophore dyes, and/or non-fluorescent proteins. This opens the possibility for the same fusion proteins observed co-localizing in microscopy to be overexpressed and purified for in vitro binding studies in FDS-SV, to provide information of number, size, and stoichiometry of complexes. Further, there is a potential for FDS-SV to be applied to more crowded solutions such as cell extracts and serum (Polling et al., 2013; Kokona et al., 2015; Hill and Laue, 2015), in which the hydrodynamic interpretation of complex sizes is less quantitative, but complex stoichiometries derived from multi-component detection should be invariant. Exploiting the switchable signal further, we have demonstrated that additional spatial and temporal modulation of the psFPs signal in FDS-SV is possible. This has the potential to further improve discrimination of different psFPs and to enhance hydrodynamic analysis, for example, in the FRAP-like configurations used in the present study.

The switchability of signal and localized optical manipulation afforded by psFPs can be envisioned to expand the toolbox of analytical ultracentrifugation in many other unexpected ways. For instance, the creation of lamella-like signal configurations within the concentration plateau region may enable novel assays, for example, to observe subunit exchange rates of size-resolved macromolecular complexes from the lamella migration and signal amplitude changes, or to study complex formation in crowded solutions within the plateau region of rapidly sedimenting co-solutes. Even though the present work was focused on SV, sedimentation equilibrium (SE) analytical ultracentrifugation would be expected to equally benefit from the use the new temporal tag: for example, once molecules are in thermodynamic equilibrium of sedimentation, psFPs may be reset or depleted, for example, by uniform 405 nm or 488 nm illumination, and the ensuing temporal signal evolution could reveal the equilibrium distribution specifically of psFPs in a mixture. Further, one could envision FRAP-like localized switching in SE to complement thermodynamic with hydrodynamic information obtained while maintaining SE. Beyond analytical ultracentrifugation, quantitatively exploiting the characteristic dynamics of photoswitching arising from different switching quantum yields may prove useful in other techniques.

The new MCMC approach we developed may be compared to other fluorescence methods used to detect binding, including fluorescence correlation/cross-correlation, polarization, proximity and life time imaging methods. These generally offer greater flexibility in solution conditions and can be carried out in vivo. However, the strongly size-dependent migration of molecules in the gravitational field is a unique feature of FDS-SV that can lead to significantly higher resolution of macromolecular complexes. We believe this has great potential for the study of systems that exhibit polydisperse mixtures of different complexes, which would elude traditional structural characterization, and only display population-averaged features in spectroscopic techniques.

Of interest, we discovered changes in the switching rate and final contrast of rsEGFP and rsEGFP2 induced by antibody binding. This suggests that subtle binding-induced conformational changes of the GFP β-barrel occur that can lead to changes in the equilibrium populations of photophysical states of the chromophore. For Dronpa, NMR studies have revealed flexibility of the β-barrel allowing non-radiative decay processes in the dark state (Mizuno et al., 2008), and viscosity-mediated reduction of flexibility has been proposed as a mechanism for the viscosity sensitivity of its fluorescence (Kao et al., 2012). Also, structural flexibility mediating conformational changes from the protein exterior to the chromophore environment inside the β-barrel has been exploited for GFP as a sensor (Berg et al., 2009). It seems conceivable that a similar mechanism may be at work in the binding sensitivity of its photoswitchable variants. Even though the psFPs will typically be designed to be an inert tag, rather than offering binding sites, this reveals the potential for an additional, more subtle source of information in temporally modulated FDS-SV, if the equilibrium of photophysical states is altered through occupation of a binding site.

Prior work on the assembly of AMPA receptor ATDs suggested an inefficient process for the formation of GluA2/GluA3 heteromers because the \( K_{d,22} \) for homodimer assembly by GluA2, 1.8 nM, was only 1.4 fold greater than the \( K_{d,23} \) of 1.3 nM for heterodimer assembly (Rossmann et al., 2011). Using the MCMC approach we find that the process is much more efficient, with a \( K_{d,23} \) for heterodimer assembly of 0.32 nM, 85-fold smaller than the 27.1 nM \( K_{d,22} \) for homodimer assembly.
by GluA2, and four orders of magnitude smaller than the $K_{d,33}$ for GluA3 homo-dimerization, which is consistent with the obligate formation of GluA2/GluA3 heterodimer in neurons (Rossmann et al., 2011).

While this first application highlights the potential of the method to determine sub-nanomolar dissociation equilibrium constants of protein complexes involving competitive or cooperative self- and hetero-association processes, other key aspects of the method are the ability to simultaneously monitor the size-distribution of individual components and their complexes formed in solution, and the potential to discriminate two or more different psFPs. The availability of size-distributions for all components distinguishes MCMC FDS-SV from methods such as SPR or ITC often used for studying bimolecular reactions. Considering that, from large-scale proteomic experiments (Gavin et al., 2002; Krogan et al., 2006), on average more than four components are in cellular protein complexes, it is necessary to develop methods that can elucidate their stoichiometries, architectures, and driving forces. We believe MCMC FDS-SV offers a powerful new approach to study such multi-component complexes in solution.

**Materials and methods**

**Analytical ultracentrifugation with fluorescence detection system (FDS)**

SV experiments were carried out in an Optima XL-A (Beckman Coulter, Indianapolis IN) equipped with an FDS (Aviv Biomedical, Lakewood NJ). The FDS light source is a 488 nm 10 mW diode laser, and emission is detected between 505 nm and 565 nm. Setup of the AUC followed standard protocols (Zhao et al., 2013b), using an 8-hole An-50 TI rotor. In order to minimize local exposure of the samples during FDS adjustment and magnet angle locking, radial calibration and PMT settings were evaluated at 3000 rpm, followed by temperature equilibration at 20˚C, and acceleration to 50,000 rpm. If initial FDS adjustment required more than a few minutes, the samples in the rotor were illuminated with 405 nm prior to temperature equilibration. With the FDS focal depth set at 4000 µm and the PMT power at 51%–80% with gain of 8 (dependent on sample concentration), sequences of radial scans were acquired continuously for 12 hr with radial intervals of 20 µm.

For passive blinking experiments, pauses in data acquisition were applied. For rapid blinking experiments a modified Optima XL-A was used, where 405 nm light from a high-power LED was guided into the rotor chamber through the interference optics port in the heat sink to illuminate the spinning rotor. A sector-shaped mask concentric to the axis of rotation was used.

**Photoswitching and exposure geometry in FDS**

The FDS signal is linear with concentration in the nanomolar concentration range and below (Zhao et al., 2013b; Lyons et al., 2013), and accordingly, we consider the fluorescence signal $F(r,t)$ a product of concentration $c(r,t)$ and a specific molar fluorescence signal increment $E$. The overall initial signal increment $c_0$ will depend, for example, on laser power, absorption coefficient, intrinsic fluorescence quantum yield, and detection efficiency. Photoswitching is modeled as a two-state process, with a single exponential transition from an initial equilibrium of photophysical states to another equilibrium after a long time of 488 nm irradiation in the FDS. The rate of transition will depend on a quantum efficiency of photoswitching and the total count of photons incident on the migrating fluorophore. The latter will be dependent on the incident laser power density, as well as the distance from the center of rotation.

Briefly, since all molecules have the same angular velocity $\omega$, they traverse a constant beam width $\delta$ more quickly at higher radii. At position $r'$ the sample has a transverse velocity $\omega r'$ and (with negligible difference between the arc and secant in the AUC geometry) molecules are illuminated for the time $\delta/\omega r'$ at each rotation. It follows that their total photon count is

$$\Phi(r,t) = \phi \int_0^t \frac{\delta}{2\pi r'(t')} dt'$$  \hspace{1cm} (1)

where $r'(t)$ is the trajectory of the molecule through the sample. Neglecting Brownian motion, the path history of particles with sedimentation coefficient $s$ found at time $t$ at position $r$ is
\[ r'(t') = re^{2\beta(t'-t)} \]  

which, after integration, leads to

\[ \Phi(r,t) = \frac{\phi}{2\pi r \nu \omega^2} \left[ e^{\omega^2 r^2} - 1 \right] \]  

as the accumulated total photon count seen by the fluorophore found at radius \( r \) at time \( t \) sedimenting with \( s \). Therefore, combining constants from illumination and molecular photoswitching into a single parameter \( \beta \), we find the time-dependent fluorescent signal increment

\[ E(s, r, t - t_{045}) = \varepsilon_0 \left( 1 + \alpha \exp \left\{ -\frac{\beta}{(r/r_0)^2} \left[ e^{\omega^2 (r/r_0)^2} - 1 \right] \right\} \right) \]  

where \( \alpha \) describes the fractional signal change after long time, and \( r_0 \) is a reference radius. The reference time-point \( t_{045} \) is the last time of fluorophore reset with strong 405 nm exposure (and \( t_{045} = 0 \) without reset illumination). The slight radial dependence causes slopes that for individual psFPs are indistinguishable from the effects of a small mismatch between the focal plane of the scanner and the plane of rotation causing small gradients of signal magnification (Zhao et al., 2013b; Zhao et al., 2014b) but for studying mixtures of psFPs they need to be quantitatively accounted for.

**Monochromatic multi-component analysis**

Analogous to the multi-wavelength sedimentation coefficient distribution analyses (MSSV) (Balbo et al., 2005), we model the evolution of experimental fluorescence scans \( a(r,t) \) as a superposition of signals from different components \( p \), each exhibiting a different unknown distribution of sedimentation coefficients \( c_p(s) \)

\[ a(r, t) = \sum p \int c_p(s) E^{(p)}(s, r, t) \chi_1(s, r, t) ds \]  

where \( E^{(p)}(s, r, t) \) denotes the temporal signal change (Equation 4), and \( \chi_1(s, r, t) \) denotes the evolution of concentration for a species with sedimentation coefficient \( s \) in the centrifugal field, as calculated by the master partial differential equation for sedimentation and diffusion in the centrifugal field, the Lamm equation (Lamm, 1929; Brown and Schuck, 2008). Sedimentation and diffusion are both governed by the same hydrodynamic frictional coefficient (Cheng and Schachman, 1955), which allows diffusion to be estimated for all species based on a hydrodynamic scaling law \( D(s) \) for particles with given translational friction coefficient (Schuck, 2000). Since \( \int f_0 \) measures the hydrodynamic extension of a particle relative to a compact sphere of the same mass and takes a narrow range of values for most folded proteins (Serdyuk et al., 2007; Cantor and Schimmel, 1980), it was fixed in MCMC. The distributions \( c_p(s) \) are calculated after discretization into a linear least squares problem with Tikhonov regularization (Balbo et al., 2005; Schuck, 2000), and implemented in the public domain software SEDPHAT (https://sedfitsedphat.nibib.nih.gov/software/default.aspx). Analogously to MSSV, the approach is compatible with mass conservation-based regularization approaches to further enhance component resolution (Brautigam et al., 2013). After determination of \( c_p(s) \), integration can be carried out to determine signal weighted-average sedimentation coefficients \( s_{p,w} \) compatible with the transport method, and further isotherm analysis of \( s_{p,w} \) as a function of protein concentrations can take place with binding models (Schuck et al., 2003, 2015). For the GluA2/GluA3 interaction analysis, the isotherm modeling was based on the competitive self- and hetero-dimerization model in SEDPHAT.

**Error analysis**

As an experimental design tool an analytical prediction of errors in the MCMC decomposition was implemented for two species with fluorophores \( p \) and \( q \) sedimenting at the same \( s \)-value, in the absence of initial localized switching. After discretization of Equation 5 and neglect of weak \( s \)-value dependence of the signals, it can be shown that, given \( n \) meaningful data points with relative error \( \delta_n \), the relative error in \( c_p \) is
\[
\delta_c = \text{cond}(E) \frac{2\delta_t}{\sqrt{n}}
\]  

, i.e., is dependent on the condition number of the matrix \( E \) where

\[
E_{p,q} = \sum_{r} E^{(p)}(t) E^{(q)}(t) w(x,t)
\]

contains the mutual products of signals at experimentally available scan times \( t \), weighted with a sedimentation term \( w(x,t) = \sum_{r} \chi_{s,r} r^2 \). Mathematically, \( E \) plays the same role as the extinction coefficient matrix in multi-wavelength analysis. Essentially, fluorophores will be distinguishable on the basis of their temporal signature if cross-terms in \( E \) are small during observed times in the sedimentation experiment.

For the error analysis of experimental data, a Monte-Carlo statistical analysis was implemented in order to determine error estimates for the distributions \( c_p(x) \) and their integrals such as \( s_w \). In the present work, 500 iterations were chosen to estimate the sensitivity of \( s_w \) to data acquisition noise, not including variation of the meniscus.

**Sedimentation model for FRAP-like SV with initial localized illumination**

In the presence of inhomogeneous illumination, the spatially uniform time-dependent extinction coefficient model of Equation 4 must be extended to account explicitly for sedimentation and diffusion of molecules in fluorescent state \( \chi_f \) and dark state \( \chi_d \). In the presence of illumination with a spatial-temporal intensity profile \( I(r,t) \) at a wavelength of 488 nm, transition from the fluorescent to the dark state occurs with a rate \( k_{f \rightarrow d}(r,t) = q_{f \rightarrow d} I(r,t) \) (assuming a quantum efficiency \( q_{f \rightarrow d} \)). The evolution of concentrations of molecules in the fluorescent and dark state is then described with the coupled Lamm equation (which may be extended similarly for the reverse transition)

\[
\frac{\partial \chi_f}{\partial t} = -\frac{1}{\rho} \left( \chi_f w(x^2 r^2 - D \frac{\partial^2}{\partial x^2} r^2 \right) - \chi_f k_{f \rightarrow d}(r,t) \\
\frac{\partial \chi_d}{\partial t} = -\frac{1}{\rho} \left( \chi_d w(x^2 r^2 - D \frac{\partial^2}{\partial x^2} r^2 \right) + \chi_d k_{f \rightarrow d}(r,t)
\]

The spatial illumination profile \( I(r,t) \) was empirically modeled as a superposition of beams with Gaussian intensity profile, accounting for the cone-shape intensity profile. The amplitudes and center radii were introduced as additional parameters refined from the fit. After initial localized illumination, spatially uniform scanning governs the further evolution of the signal of the fluorescent species and \( E(s,x,t) \times \chi_f(r,t) \) can be inserted in the multi-component decomposition of Equation 5.

Modeling the coupled sedimentation/diffusion/photoswitching process will account for sedimentation and diffusion that takes place during strong illumination, which causes the precise shape of the trough to slightly depend on the rates of macromolecular sedimentation and diffusion. However, the initial exposure is precisely identical for all different samples in the rotor. With this approach, the precise initial illumination profile is inconsequential because the parameters of interest are only in the further evolution with time.

**Protein expression and preparation**

The plasmid pQE31-rsEGFP was kindly provided by Stefan Jakobs (Max Planck Institute for Biophysical Chemistry). The plasmid rsEGFP2 was produced by mutating the pQE31-rsEGFP plasmids using following primers, T65A (5'-CCACCCTGGCGCTACGCGTG-3'), A150V (5'-GCCACAACGTCTATATCATGG-3'), and N205S (5'-GCACCCAGTCCAAGCTGAC-3'). Mutations are underlined. The plasmid pQE31-Padron was also provided by Stefan Jakobs and EGFP was expressed from the pRSETA-EGFP plasmid both described previously (Zhao et al., 2014b).

The GluA2 ATD cDNA, residues Met1–Ser404, was cloned into the pRK5-ires-EGFP mammalian expression vector with a C-terminal LELVPRGS-His8 linker, thrombin cleavage site and affinity tag. The rsEGFP–GluA3 ATD fusion construct was created as follows: The cDNA for the GluA3 signal peptide residues Met1–Gly22, followed by an SGSG tetrapeptide linker, was inserted upstream of the cDNA for rsEGFP residues Val2–Lys239, and connected by an SGS tripeptide linker to the cDNA for GluA3, residues Gly23–Ser408, followed by a C-terminal LELVPRGS-His8 linker, thrombin cleavage site and affinity tag, cloned into the pRK5 mammalian expression vector. Both constructs were
expressed in HEK293T cells by transient transfection of suspension cultures using PEI MAX 40000 (Polysciences Inc.). The secreted constructs with native complex glycosylation were concentrated by ultrafiltration using Pellicon 10 kDa MW cutoff cassettes (Millipore) and purified by immobilized metal affinity chromatography using a HiTrap NTA column (GE Healthcare), followed by proteolysis with thrombin, and then ion exchange chromatography using a HiTrap Q column (GE Healthcare). The pooled fractions were concentrated and then dialyzed against AUC or labeling buffer as appropriate (150 mM NaCl, 1 mM EDTA, 20 mM NaPhosphate, pH 7.5 and 7.0 respectively).

A 14.4 μM concentration of purified GluA2 ATD was mixed with a 12 M excess of N-hydroxsuccinimide (NHS) ester–activated Dylight488 (Thermo Fisher Scientific) dissolved in DMSO and then diluted with labeling buffer. The reaction was incubated in the dark at room temperature for 45 min and then loaded onto a high resolution size exclusion chromatography column (Superdex 75 10/300 GL) equilibrated with AUC buffer to separate free dye from labeled protein. The protein concentration and labeling ratio were then determined by UV-Vis spectrophotometry using values for ε_{280} of 55,720 M⁻¹cm⁻¹ for the unmodified protein, ε_{280} of 10,290 M⁻¹cm⁻¹ and ε_{493} of 70,000 M⁻¹cm⁻¹ for Dylight488.

Bovine serum albumin (BSA) was acquired from Sigma Aldrich (catalog#A7030, St. Louis) and fluorescently labeled with FITC using the labeling kit from Thermo Fisher targeting the primary amine on BSA (catalog#53027). Monoclonal anti-GFP IgG (D153-3) was purchased from MBL International (Woburn, MA) and subjected to exhaustive dialysis with the working buffer, phosphate buffered saline (5.62 mM Na₂HPO₄, 1.06 mM KH₂PO₄, 154 mM NaCl, pH 7.40). To all samples, unlabeled BSA was added at 0.1 mg/ml to suppress surface adsorption of the proteins of interest.

**Fluorescence spectroscopy**

Benchtop fluorescence spectroscopy experiments were carried out in a Fluorolog spectrofluorometer (Horiba Instruments Inc., Irvine CA). rsEGFP or rsEGFP2 at were studied at a final concentration of 0.5 μM in the presence or absence of equimolar anti-GFP antibody, after 2 hr incubation of the mixture. Emission spectra were collected with slit widths set to 1 nm. For kinetic experiments of photoswitching, the 490 nm excited 508 nm fluorescence of rsEGFP or the 483 nm excited 502 nm fluorescence of rsEGFP2 was monitored, respectively.

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**Author contributions**

HZ, Conceived of the method, Designed and carried out the AUC experiments, Implemented computational analysis, Drafting or revising the article; YF, Designed and carried out the benchtop fluorescence experiments, Analysis and interpretation of data; CG, Designed fluorescent proteins and carried out protein expression and purification, Contributed unpublished essential data or reagents; EJAA, Carried out protein expression and purification, Contributed unpublished essential data or reagents; MLM, Designed fluorescent proteins and carried out protein expression and purification, Drafting or revising the article, Contributed unpublished essential data or reagents; GP,
Designed fluorescent proteins and carried out protein expression and purification. Designed and carried out the benchtop fluorescence experiments, Drafting or revising the article, Contributed unpublished essential data or reagents; PS, Conceived of the method, Designed and carried out the AUC experiments, Implemented computational analysis, Wrote the manuscript

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