Research Article

Lattice Boltzmann Simulation of Airflow and Mixed Convection in a General Ward of Hospital

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In the present investigation the airflow and heat transfer for mixed convection have been simulated for a model general ward of hospital with six beds and partitions using the Lattice Boltzmann Method (LBM). Three different Reynolds numbers 100, 250, and 350 have been considered. Bounce-back condition has been applied at the wall. Results have been represented in three different case studies and the changes have been discussed in terms of streamlines and isotherms. Code validation has also been included before going through the simulation process and it shows good agreement with previously published papers when the comparison is made on average Nusselt number. Results show that the pattern of indoor airflow is varied in each and every case study due to the effect of mixed convection flow and placement of partition. In addition, the changes in average rate of heat transfer indicate that patients closer to inlet get the most air and feel better and if any patient does not need much air, he or she should be kept near the outlet to avoid temperature related complications.

1. Introduction

The study of mixed convection fluid flows has become an attention-grabber due to considerable practical interest in many engineering applications, such as nuclear reactors [1], crystal growth, solar collectors [2], and reservoirs and lakes [3]. Apart from these, mixed convection appears to be a concerning issue while designing modern ventilation system in high-rise buildings and health care centers. The main purpose of room air-ventilation system is to provide comfortable and good indoor air quality with minimum energy consumption so that the residents inside do not feel stuffy or uncomfortable. So, to design efficient ventilation system, necessary designing or simulation tools are required in order to accurately visualize the airflow pattern and know the appropriate positions of inlets and outlets in any complex geometry.

The combined effect of natural and forced convection in fluid flows has been analyzed by many researchers over decades. The fact behind their curiosity lies in the buoyancy effect that can be the dominant factor in determining heat transfer. Since experimental scale modeling is very expensive, researchers continued their study with the aid of traditional Computational Fluid Dynamics (CFD) model simulation technique. But the main problem with this traditional method involves solving the Navier-Stokes (NS) equations that need more CPU time and memory. Researchers found that the solution lies in the Lattice Boltzmann Model (LBM), an alternative Computational Fluid Dynamics (CFD) model that does the same job by solving discrete Boltzmann equation which is a faster process than solving the NS equations [4]. LBM has originated from Lattice Gas Automata (LGA) [5] which is used to simulate fluid dynamics by tracing the movement of single-particle distribution function considering the space, time, and particle velocities to be discrete.

The reasons behind LBM’s popularity are as follows: because it has simple mathematical modeling of any complex system, the boundaries are treated in simple manner, it is a suitable model for parallel computation, and, apparently, it saves 30 percent of the total CPU time which would have been occupied by nonlinear Riemann problem in CFD [6]. LBM is also considered to be very easy and efficient method over finite volume, finite-difference, and finite element techniques. Many experiments and researches were performed to explore the effectiveness of LBM. Peng et al. [7] simplified thermal
LBM to study incompressible thermal flows. Lee et al. [8] researched the incompressible lattice Boltzmann (LBM) model to simulate axisymmetric geometry. Sidik [9] calculated the temperature field and velocity field utilizing two different distribution functions for each field and developed an incompressible 2D and 3D thermohydrodynamics for the LBM. The main aim of Mondal and Li's [10] investigation was to observe the effect that volumetric radiation has on the natural convection in a square cavity containing an absorbing, emitting, and scattering medium. Suzuki and Suchy [11] studied a method concerning local viscosity changes in single-relaxation time (SRT) LBM. Moreover, LBM was successful in various fluid dynamical problems including flows in porous media [12], magnetohydrodynamics [13], immiscible fluids [14], and turbulence [15]. LBM can also be applied to investigate indoor airflow. In 2002, Crouse et al. [16] were the first and probably the only ones to implement LBM in indoor convective airflow analysis.

An investigation was carried out by Zhang et al. [17] who studied the airflow inside an airliner ward performing experimental mathematics and numerical simulations. The ward was assumed to be half occupied with 28 seats and twin-aisle. The authors used the Reynolds averaged Navier-Stokes equations based on the RNG \( k-\epsilon \) model to solve the air velocity, air temperature, and gas contaminant concentration and applied a Lagrangian technique to model the particle transport. The numerical results showed good agreement quantitatively with their experimental data. However, they confessed that it is very challenging and difficult to achieve a complete and accurate validation for the complex flow in a ward. Later, Zhang and Lin [18] used LBM to analyze indoor airflows. They worked on low Reynolds number indoor airflow fields in a model room building a partition and their computational results of LBM were found to be in agreement with the experimental data in terms of airflow velocities. They applied LBM in a relatively more complex environment, that is, a model ward with 10 beds. Although their works were solely on fluid flow, they did not consider any temperature equation.

Liu et al. [19], on the other hand, utilized CFD to examine a critical issue of hospital Operating Room (OR). They numerically simulated a horizontal airflow to control airborne particles inside a hospital OR. The investigation was performed on different horizontal airflow patterns and air quality inside an OR model of dimension 300 cm \( \times \) 296 cm \( \times \) 240 cm. They realized the urgency of a proper ventilation system inside a hospital OR and, so, carried on some onsite tests and CFD simulations to estimate the effectiveness of latitudinal unidirectional airflow in order to bring down infectious airborne particles. The suggested ventilation supplying ultraclean air from a horizontal plane avoided obstacles, like medical lights from upstream flow, and also lateral flow perpendicular to the airflow of thermal plume around surgeons and patient can avoid opposing effect between the two airflows in downward airflow system. However, the application of airflow in horizontal direction had not been properly examined in their paper.

All the above examples verified the capability and effectiveness of LBM over traditional CFD, but the experiments were done either considering a natural fluid flow or forced fluid flow, whereas in reality the presence of both flows can be seen simultaneously. In purely natural convection flow, the only driving force is the density gradient, and for forced convection the force is inflow condition or pressure-gradient. Since there is temperature difference between all objects, living beings, and the environment, in the presence of a gravitational field temperature gradients tend to induce density gradients that ultimately drives the fluid flow. Watzinger and Johnson [20] took the first initiative to investigate heat transfer in a turbulent mixed convective water flow, both for opposing and supporting flow conditions. Later, Prasad and Koseff [21] investigated the combined natural and forced convection heat transfer in a deep lid-driven cavity flow. Hongtau Xu et al. [22] numerically studied double diffusive mixed convection around a heated cylinder in an enclosure and Al-Sanea et al. [23] analyzed the effect of input Reynolds number and room aspect ratio on turbulent flow and ceiling transfer coefficient for mixed convection using CFD method. Zhao et al. [24] used traditional CFD method to investigate three-dimensional (3D) nonlinear multiple steady fluid flows in a slot-ventilated enclosure. Kefayati et al. [26] applied finite volume method to experiment with a fluid-saturated porous medium on mixed convection flow in a lid-driven enclosure. On the other hand, Kefayati et al. [26] applied LBM to simulate magnetohydrodynamic mixed convection inside a lid-driven square cavity with linearly heated wall. As the present investigation is based on mixed convection inside a hospital ward having partition in the middle, the work of Lee and Awbi [27] is worth mentioning which is on the effect of room air quality with mixing ventilation due to internal partitioning, but their observation was only on statistical analysis using traditional CFD codes. They stated that to get better room air quality the partition positioned towards the exhaust zone having a larger height and gap underneath was beneficial.

The purpose of the present work is to focus on indoor airflow simulation by LBM in a hospital ward with six beds and partitions. The airflow inside the ward is considered to be mixed convection flow and different cases have been considered as well. The room temperature has been kept lower than patients’ temperature as each patient on bed has been considered to release heat continuously in the proposed model. Before going through further simulation, code validation has been presented. This paper is organized in the following way: in Section 2, physical geometry of the problem has been discussed, followed by the mathematical formulation in Section 3. In Section 5, the results have been discussed in detail and then conclusion has been added to Section 7.

2. Physical Geometry

The present investigation has been applied for the mixed convection in a general ward of hospital, as shown in Figure 1. In Figure 1(a), it is just a ward without any bed or partition; in Figure 1(b), a general ward with six model beds is shown and in Figure 1(c) that ward with six beds along with a partition is depicted. Here, \( h \) is the height and \( l = 2h \) is the horizontal length of each block and the height and width of the partition
3. Mathematical Formulation

The LBM was originated from Ludwig Boltzmann’s kinetic theory of gases. The basic theory of this equation is that gases or fluids can be imagined as consisting of a large number of tiny particles moving with random motion. The exchange of momentum and energy is found through particle streaming and collision between particles. So, this process can be demonstrated by the Boltzmann transport equation [28, 29]:

\[
\frac{\partial f}{\partial t} + \vec{u} \cdot \nabla f = \Omega(f, f^{eq}),
\]

where \( f^{eq} \) is the equilibrium distribution function, respectively, \( \vec{u} \) is the particle velocity, and \( \Omega \) is the collision operator. Here, \( f \) represents \( f(\vec{x}, e_i, t) \) which is the probability to locate a particle at position \( x \) with velocity vector \( e_i \) at time \( t \).

3.1. Lattice Boltzmann Method. The LBM simplifies Boltzmann’s original idea of gas dynamics by reducing the number of particles and circumscribing them to the nodes of a lattice. For a two-dimensional model, a particle is preferred to stream in one of 9 directions, including the one staying at rest. For this type of modeling, the most popular one is \( D2Q9 \) model which has been considered in this work. This is the standard model for two-dimensional structures for both flow and temperature conditions. The velocities for these conditions are known as macroscopic velocities.
The discretized Lattice Boltzmann (LB) equations for both flow and temperature field can be written as follows [29]:

\[
\begin{align*}
    f_i(\vec{x} + \delta \vec{e}_i, t + \delta t) - f_i(\vec{x}, t) &= -\frac{1}{\tau_y} \left[ f_i(\vec{x}, t) - f_i^{(eq)}(\vec{x}, t) \right] + \delta t \cdot F_i, \\
    g_i(\vec{x} + \delta \vec{e}_i, t + \delta t) - g_i(\vec{x}, t) &= -\frac{1}{\tau_\alpha} \left[ g_i(\vec{x}, t) - g_i^{(eq)}(\vec{x}, t) \right].
\end{align*}
\]

(2)

Here, \( \tau_y = 3\nu + 0.5 \) and \( \tau_\alpha = 3\alpha + 0.5 \) are the single-relaxation times that control the rate of approach to equilibrium, \( f_i(\vec{x}, t) \) and \( g_i(\vec{x}, t) \) are the density distribution functions for velocity and temperature, respectively, along the direction \( \vec{e}_i \) at \( (\vec{x}, t) \), \( \nu \) is the kinematic viscosity, and \( \alpha \) is the thermal diffusivity. The particle speed is \( \vec{e}_i \) and \( \rho \) is the density.

To calculate the equilibrium distribution functions for the velocity, \( f_i^{(eq)}(\vec{x}, t) \), and for the temperature, \( g_i^{(eq)}(\vec{x}, t) \), the general expressions have been considered [29–31]:

\[
\begin{align*}
    f_i^{(eq)} &= w_i \rho \left[ 1 + \frac{3(\vec{e}_i \cdot \vec{u})}{c^2} + \frac{9(\vec{e}_i \cdot \vec{u})^2}{2c^4} - \frac{3(\vec{u} \cdot \vec{u})}{2c^2} \right], \\
    g_i^{(eq)} &= w_i T \left[ 1 + \frac{3(\vec{e}_i \cdot \vec{u})}{c^2} + \frac{9(\vec{e}_i \cdot \vec{u})^2}{2c^4} - \frac{3(\vec{u} \cdot \vec{u})}{2c^2} \right],
\end{align*}
\]

(3)

where \( \vec{u} = (u, v) \) is the fluid velocity and \( c = \Delta x / \Delta t = 1 \) is the lattice speed. The weighting factors \( w_i \) for D2Q9 are given as [29]

\[
w_i = \begin{cases} 
    \frac{4}{9}, & i = 0 \\
    \frac{1}{9}, & i = 1, 2, 3, 4 \\
    \frac{1}{36}, & i = 5, 6, 7, 8.
\end{cases}
\]

(4)

The macroscopic fluid density \( \rho \) and velocity \( \vec{u} \) are obtained from the moments of the distribution function as follows [28]:

\[
\begin{align*}
    \rho(\vec{x}, t) &= \sum_{i=0}^{8} f_i(\vec{x}, t), \\
    \vec{u}(\vec{x}, t) &= \frac{1}{\rho(\vec{x}, t)} \sum_{i=0}^{8} \vec{e}_i f_i(\vec{x}, t)
\end{align*}
\]

(5)

and the temperature \( T \) is obtained as [32]

\[
T = \sum_{i=0}^{8} g_i(\vec{x}, t).
\]

(6)

3.2. Boundary Conditions. Boundary conditions (BCs) are very important for both the stability and the accuracy of any kind of numerical solution. For LB modeling, the discrete distribution functions on the boundary need to be taken care of to reflect the macroscopic BCs of the fluid. In this work, at the wall, the bounce-back condition has been applied.

Bounce-back BCs are usually used to implement no-slip conditions on the boundary. By the bounce-back condition, it is meant that when a particle of a certain fluid for discrete distribution function reaches a boundary node, the particle will scatter back to the fluid along with its incoming direction. Bounce-back condition can be of various types but on-grid bounce-back condition has been used in this paper.

3.2.1. Boundary Condition for Velocity. Four possible directions in two-dimensional structure—east, west, north, and south—have been considered in the proposed model and no-slip or bounce-back boundary condition is used at the walls, which has been shown in Figure 1.

At east (right), west (left), and south (bottom) walls the bounce-back condition has been applied and the resulting relations are given below in order:

\[
\begin{align*}
    f_3 &= f_1, \\
    f_7 &= f_5, \\
    f_6 &= f_8, \\
    f_1 &= f_3, \\
    f_5 &= f_7, \\
    f_8 &= f_6, \\
    f_2 &= f_4, \\
    f_5 &= f_7, \\
    f_6 &= f_8.
\end{align*}
\]

(7)

On the other hand, at the north (top) wall, three different boundary conditions have been applied. At the inlet, Zou and He boundary conditions have been applied as shown in the following [33]:

\[
\begin{align*}
    \rho_N &= \frac{(f_0 + f_1 + f_5 + 2(f_2 + f_6 + f_3))}{(1 + U)}, \\
    f_4 &= f_2 - \frac{2}{3} \rho_N U, \\
    f_8 &= f_6 - \frac{1}{6} \rho_N U, \\
    f_7 &= f_5 - \frac{1}{6} \rho_N U,
\end{align*}
\]

(8)

where \( U \) is the bulk velocity based on the Reynolds number \( \text{Re} = UH / \nu \). At the outlet the following boundary conditions are used:

\[
\begin{align*}
    f_{4_N} &= f_{4_N-1}, \\
    f_{8_N} &= f_{8_N-1}, \\
    f_{7_N} &= f_{7_N-1}.
\end{align*}
\]

(9)
and bounce-back condition is used for the rest of the top walls. At the top surface and at each side of a block and partition, the following bounce-back conditions have been used:

**Top surface:**

\[ f_{2,x_i} = f_{4,x_i}, \]
\[ f_{5,x_i} = f_{7,x_i}, \]
\[ f_{6,x_i} = f_{8,x_i}, \]

\[ f_{7,x_i} = f_{5,x_i}, \]

**Left side:**

\[ f_{1,x_i} = f_{3,x_i}, \]
\[ f_{5,x_i} = f_{7,x_i}, \]
\[ f_{8,x_i} = f_{6,x_i}, \]

**Right side:**

\[ f_{3,x_i} = f_{1,x_i}, \]
\[ f_{6,x_i} = f_{8,x_i}, \]

\[ f_{7,x_i} = f_{5,x_i}, \]

3.2.2. Boundary Condition for Temperature. Cold and hot temperature conditions are applied at the walls (see Figure 1).

At east (right) wall the cold temperature condition is \( g_3 = -g_1, g_7 = -g_5 \), and \( g_6 = -g_8 \).

At west (left) wall the cold temperature condition is \( g_1 = -g_3, g_5 = -g_7 \), and \( g_6 = -g_8 \).

At south (bottom) wall the cold temperature condition is \( g_2 = -g_4, g_5 = -g_7 \), and \( g_6 = -g_8 \).

At the north (top) wall in the outlet a zero gradient boundary condition is applied as follows:

\[ g_{4, N} = g_{4, N-1}, \]
\[ g_{6, N} = g_{6, N-1}, \]
\[ g_{7, N} = g_{7, N-1}. \]

And the rest of the top wall is kept cold by using the conditions \( g_4 = -g_2, g_6 = -g_8 \), and \( g_7 = -g_5 \).

At the top surface of each block the hot temperature condition is used as follows:

\[ g_{2, y_2} = T_w (w_2 + w_4) - g_{4, y_2}, \]
\[ g_{5, y_2} = T_w (w_5 + w_7) - g_{7, y_2}, \]
\[ g_{6, y_2} = T_w (w_6 + w_8) - g_{8, y_2}, \]

where \( y_2 \) indicates the top surface of the blocks and \( T_w \) is the wall temperature.

3.3. Nondimensional Number and Mixed Convection Parameter. The important nondimensional number Grashof (Gr) and Prandtl (Pr) numbers are defined as [32]

\[ \text{Gr} = \frac{\beta G_f H^3 (T_H - T_C)}{\nu^2}, \]

\[ \text{Pr} = \frac{\nu}{\alpha}. \]

In the mixed convection the Richardson number, \( \text{Ri} \) defined as \( \text{Gr} / \text{Re}^2 \), controls the flow phenomena. In this simulation the force term is defined as follows [34]:

\[ F = 3 \omega_i \text{Ri} (T - T_m) e_y, \]

where \( T_m = (T_H + T_C) / 2 \) is the mean temperature. In this paper the fluid velocity \( \mathbf{u} \) is nondimensionalized by the constant inlet velocity \( \mathbf{U} \) and the nondimensional temperature is \( \theta = (T - T_c) / (T_w - T_c) \).

In the present work, the Mach number (Ma) for Re = 100 is 0.05, for Re = 250 is 0.02, and for Re = 350 is 0.014. All these values are less than 0.3 which satisfy the condition of incompressible fluid flow [32]. In buoyant flow, Mach number and thermal diffusivity (\( \alpha \)) can be defined by the following equations after fixing the values of viscosity, Prandtl number, and Reynolds number:

\[ \text{Ma} = \frac{\nu \sqrt{\text{Gr}}}{N_c}, \]

\[ \alpha = \frac{\nu}{\text{Pr}}. \]

4. Convergence Criteria

Standard LBM, being explicit time-marching in nature, requires a long time to attain steady state convergence. However, convergence of solution is one of the highlights of the procedure of recovering the Navier-Stokes equations from LBM. In this single-relaxation-time LBM, the iterative procedure is terminated when the velocity and temperature field satisfy the following convergence criteria:

\[ \sum |\phi^{(n+1)} - \phi^{(n)}| < 10^{-9}, \]

where \( \phi \) is the velocity \( \mathbf{u} \) or temperature \( T \) and \( n \) is the iteration index and the sum is over the whole domain.

5. Results and Discussions

This section has been divided into four subsections. At first, code validation has been performed for different values of Re and has been compared in tabular format. In the consequent three subsections, three case studies have been considered inside the hospital ward. In all three cases, one inlet, one outlet, and six beds have been considered. Simulations have been carried out by placing one partition and later two partitions in the room while observing the indoor airflow.
Table 1: Comparison of average Nusselt numbers of present work with other investigations for Gr = 100 and Pr = 0.71.

| Re  | Ri   | Present | [35]   | [25]   | [36]   | [37]   | [38]   | [39]   | [26]   |
|-----|------|---------|--------|--------|--------|--------|--------|--------|--------|
| 100 | 0.01 | 1.917965| 1.94   | 2.01   | 2.02   | 1.985  | 2.10   | 2.09   |
| 400 | 0.00062| 3.789101| 3.84   | 3.91   | 4.01   | 3.875  | 3.85   | 4.0246 | 4.08082|
| 1000| 0.0001| 6.339137| 6.33   | 6.33   | 6.42   | 6.345  | 6.33   | 6.48423| 6.54687|

5.1. Code Validation. For code validation process, one test case is the mixed convection in a lid-driven square cavity flow for Re = 100, 400, and 100 and Gr = 100 has been considered. The present results in terms of the average Nusselt number have been compared quantitatively with the available results published in different articles that are demonstrated in Table 1. The comparison reveals a very good agreement. The results were compared with the works of Iwatsu et al. [35], Tiwari and Das [38], Kefayat et al. [26], Khanafer et al. [36], Abdelkhalek [37], Khanafer and Chamkha [25], and Waheed [39].

5.2. Case Study I: Six Beds without Partition in the Ward. In the first case study, six beds without partition have been considered. Each bed is of the same dimension. However, beds are represented as blocks in Figure 1. For the whole computational domain a lattice size of $(400 \times 50) \sim (x \times y)$ has been taken in all simulations. Each block of $(20 \times 10) \sim (x \times y)$ lattice size is used in the ward. The beds are uniformly distributed in one row. Inlet and outlet have been placed vertically on the ceiling on the left and right corners, respectively. The width of both the inlet and the outlet has been kept from 0 to 15 lattices and from 385 to 400 lattices, respectively.

Figures 2(a)–2(c) show the streamlines appended on $u/U$ velocity contour of the airflow that enters the ward through the inlet and flows out through the outlet for Re = 100, 250, and 350, respectively. In case of Re = 100, small recirculations are seen between the blocks and also near the walls in the east and west sides of the ward due to bounce-back condition. A comparatively large recirculation is formed in immediate right to the inlet that is near the top wall. For increasing Re the length of the recirculation zones increases. As shown in Figure 2, the highest value of $u/U$ is 1.08 and the lowest value is −0.14 for Re = 100. In case of Re = 250 and 350, the maximum values increase to 1.26 and 1.30, respectively. As Re increases, the inertia force of air increases which makes it easier to flow around in the ward and, hence, more heat will be transferred out through the outlet.

Figure 3 represents the isotherms of the room. As can be seen from the simulation result, only the top surface of each block is kept heated while the gaps between the blocks are cold. The heated portion of the blocks represents patients on beds who are releasing heat continuously.

Different velocity patterns have been shown in Figures 4(a)–4(n) demonstrating the $u/U$ velocity profiles at different positions of $x/H$ for the three different Re.
outlines the speed at which the air is flowing inside the ward. Due to the recirculation near the inlet, the velocity profiles are also seen to increase resulting in a bent-shaped plot in Figures 4(b) and 4(c). After $x/H = 3.5$ onwards the graphs are almost the same as there the flow characteristics are almost similar, except for Figure 4(n) which is slightly bent at the top forming because at this point the air is preparing to go through the outlet.

5.3. Case Study II: Six Beds with One Partition. In this investigation, the previous model has been updated by adding a partition in the middle of the general ward while all other

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Figure 3: Isotherms of Case I for (a) $Re = 100$, (b) $Re = 250$, and (c) $Re = 350$.

Figure 4: $u/U$ velocity profiles in Case I for the different $Re$ at different positions of horizontal locations (a) $x/H = 0.5$, (b) $x/H = 1$, (c) $x/H = 1.5$, (d) $x/H = 2$, (e) $x/H = 3$, (f) $x/H = 3.5$, (g) $x/H = 4$, (h) $x/H = 4.5$, (i) $x/H = 5$, (j) $x/H = 5.5$, (k) $x/H = 6$, (l) $x/H = 6.5$, (m) $x/H = 7$, and (n) $x/H = 7.5$. 
schematic measurements have been kept the same, as shown in Figure 1. The lattice size of partition is \((5 \times 40) \sim (x \times y)\) and it is placed just after the first three blocks (beds). Simulations have been carried out for the same three Reynolds numbers. After placing a partition just like in Figure 5, recirculation is seen in Figure 5 and it shows much better result than the previous simulations. The airflow pattern is clearer this time which shows that air moves inward smoothly, passes the partition naturally without overlapping it, and nicely flows out through the outlet creating its usual recirculation near the inlet, between the blocks and near the outlet. Unlike earlier, the recirculations now are larger and more frequent, particularly after crossing the partition. For \(Re = 100\), a large air circulation can be noticed between blocks 4 and 5 and in case of \(Re = 250\), an even larger recirculation has appeared between blocks 5 and 6 along with a newly emerged one just beside the outlet. As for \(Re = 350\), with the increase in convective air current more chaotic flow dynamics can be noticed before the partition appears. The airflow pattern in this region indicates that, in case of mixed convection for \(Re = 350\), the air stays in transitional state which shows both the laminar characteristics of natural convection and the turbulent nature of forced convection, thereby representing forced convection. Moreover, after placing the partition, the peak values of the contour have risen to 2.15 from 1.08, 2.33 from 1.26, and 2.38 from 1.30 for \(Re = 100\), \(Re = 250\), and \(Re = 350\), respectively.

Figure 6 presents the isotherms for this situation. Like in previous case, here also the topsurfaces of the blocks are kept heated to represent patients on beds and the spaces between
the blocks along with the partition are kept cold. The presence of the partition does affect the airflow characteristics as well as heat transfer phenomenon, which has been discussed in detail in the heat transfer part. Pr remains the same.

In Figure 7, the $U$ velocity profiles at different locations of $\frac{x}{H}$ are discussed for the same three Re. This time the results show more curvy lines throughout the whole experiment due to the obstacle caused because of the partition. One of the obvious differences worth mentioning is in Figure 7(g) when the air faces the partition. At this point, a long vertical line with a narrow parabolic curve at the top is shown representing the height of the partition whereas the curved part illustrates that the air is crossing the partition. Even in Figure 7(h), the graph still maintains its parabolic shape and continues this pattern throughout till the end. Another noticeable change can be seen in Figures 7(j), 7(k), and 7(l), at $\frac{x}{H} = 5.5$, $\frac{x}{H} = 6$, and $\frac{x}{H} = 6.5$, respectively, where the bends are more irregular than the previous case. This is because at these locations large recirculations have formed due to the partition, as shown in Figure 5.

According to the $U$ and $V$ centerline velocity distribution plots in Figures 8(a) and 8(b), respectively, there is a constriction in the middle of graph. This represents the partition that actually works like a wall where the velocity plots cease, just like the vertical walls in the extreme left and right sides. One possible advantage of this partition is that the airflow can be controlled if the air enters with a high speed through the inlet. Also it is noticeable in Figures 8(a) and 8(b) that, unlike the previous case, the partition helps to maintain the air velocity at a constant level until it exits out through the outlet. The $V$ velocity still drops to negative range from zero at the beginning due to downward fall of air through the inlet and ascends to zero again where it maintains its constant velocity. The graphs are more chaotic after crossing the partition due to the recirculations shown in the contour map. The temperature plot in Figure 8(c) starts just like that of the previous situation, but this time instead of becoming constant after a certain level, the graph climbs up the partition, crosses it, and then drops again, eventually decreasing to zero at $\frac{x}{H} = 8$. The rise of airflow against the partition also results in the increase in temperature at this point, therefore, the steep in the figure.

5.4. Case Study III: One Inlet and One Outlet with Two Partitions. This case study has been investigated by further modifying the proposed model adding another partition in the ward. It was done to keep patients from being exposed into more air. Each partition is placed every after two blocks (beds). Both the partitions are of the same dimension, that is, $(5 \times 40) \sim (x \times y)$ lattice size, and all other measurements are kept the same as previous situations. Simulations and analysis of this case have also been carried out for the same three Re values. Streamlines pattern of Figure 9 obtained after adding another partition shows that the size and the number of recirculations increase more than the last observation. Unlike Case II, now two large recirculations have formed...
for the corresponding experiments with each Re. Even the maximum and minimum legend values have become wider than the previous situation; for example, for Re = 100 the 2.15 value has increased to 2.37. For Re = 250 and Re = 350 the uppermost values have risen to 2.47 and 2.52 from 2.33 and 2.38, respectively. Due to bounce-back condition, the air is now forming more recirculations against the walls and between the blocks. This augmentation of values and recirculations due to buoyancy effect is visible for every increment of Re values and addition of obstacles such as partition.

The generated results of isotherms in Figure 10 give a visual idea how the heat is transferred from the blocks and passes through the outlet. Like the other cases, only the surfaces of the blocks are heated to be considered as patients who are continuously releasing heat. Everything remains the same like previous cases.

Figure 11 provides the U velocity profiles for different positions of x. According to this the graph characteristic for a partition can be seen in Figure 11(e) at x = 3 and Figure 11(j) at x = 5.5, indicating the presence of partitions at these two locations. Apart from this, at x = 5 and 7.5 in Figures 11(i) and 11(n), respectively, the parabolic shapes are more curvy than the profiles at other positions caused due to recirculations in vector plots of Re = 250 and Re = 350.
Figure 10: Isotherms of Case III for (a) Re = 100, (b) Re = 250, and (c) Re = 350.

Figure 11: u/U velocity profiles in Case III for the different Re at different positions of horizontal locations (a) x/H = 0.5, (b) x/H = 1, (c) x/H = 1.5, (d) x/H = 2, (e) x/H = 3, (f) x/H = 3.5, (g) x/H = 4, (h) x/H = 4.5, (i) x/H = 5, (j) x/H = 5.5, (k) x/H = 6, (l) x/H = 6.5, (m) x/H = 7, and (n) x/H = 7.5.

Figures 12(a) and 12(b) illustrate U and V velocity distribution curves in mid-y and Figure 12(c) shows the temperature profile at mid-y. All of these three plots have one thing in common that is also different than the previous case. In these plots there are two constrictions, instead of one, where the velocities or the temperature curve ceases. This is the location where the two partitions are present. But after crossing these obstacles the respective graphs continue until x = 8. The temperature plot in Figure 12(c) has now two steep regions due to the partitions.
For the first investigation, both the individual and average Nu obtained in Table 2 show a rising trend for each increasing Re. Since block 1 is the nearest to the inlet, it always has the highest rate of heat transfer while block 6 has the lowest value as it is located farthest from the inlet.

After placing the partition in the middle, the rate of heat transfer shown in Table 3 changes dramatically. Like Table 2, the patient at block 1 is releasing most heat for all three Re and it keeps reducing until block 5. At block 5, the values of both individual Nu and total Nu increase for Re = 250 and Re = 350, but for Re = 100, this type of airflow pattern is seen at block 4. The large recirculations were seen earlier in Figure 5. For Re = 100, recirculation is more over block 4 and that is the reason why, at block 4, individual Nu and total Nu have greater values than those of Re = 250 and Re = 350. Nu is 1.5341 at block 4 and, for the same block, these values are 1.3628 and 1.4032, respectively, for Re = 250 and Re = 350. On the other hand, if Nu at block 5 are observed, Re = 250 and Re = 350 lead the race. As per Table 3, Nu are 2.0111, 2.1598, and 2.7535 for three Re. The spike in the values of Re = 250 and Re = 350 was due to chaotic flows over block 5 in Figure 5. If changes in total Nu are observed, the values increase rapidly for an increase in Re.

For Case Study III, the shape of recirculation gets bigger due to increased Re. Above block 1, the recirculation zone comes into view and, due to that reason, Nu has the biggest edge in this situation. But as the air has tendency to pass the first partition, it moves slightly upward and that is why patient at block 2 is getting less airflow. The heat transfer rate also falls. After passing the first partition, the airflow gets its space and leads to recirculation near block 3 for Re = 100. Meanwhile, for Re = 250 and Re = 350, patients on block 4 get most air. More air means more heat transfer and that is
Table 2: Summary of average Nusselt numbers $\overline{Nu}$ for six blocks individually and in total for three Reynolds numbers at $Pr = 0.71$ in case of without partition.

| Re  | Block 1 | Block 2 | Block 3 | Block 4 | Block 5 | Block 6 | $\overline{Nu}$ (total) |
|-----|---------|---------|---------|---------|---------|---------|--------------------------|
| 100 | 3.0164  | 2.0366  | 1.7990  | 1.6667  | 1.5695  | 1.4486  | 11.5368                  |
| 250 | 4.6238  | 2.9266  | 2.2996  | 2.1784  | 2.0573  | 1.8028  | 15.8885                  |
| 350 | 5.4359  | 2.0344  | 2.4841  | 2.2300  | 2.1352  | 1.7329  | 17.5970                  |

Table 3: Summary of average Nusselt numbers $\overline{Nu}$ for six blocks individually and in total for three Reynolds numbers at $Pr = 0.71$ in case of with partition.

| Re  | Block 1 | Block 2 | Block 3 | Block 4 | Block 5 | Block 6 | $\overline{Nu}$ (total) |
|-----|---------|---------|---------|---------|---------|---------|--------------------------|
| 100 | 3.2979  | 2.0344  | 1.6115  | 1.5341  | 2.0111  | 1.6124  | 12.1014                  |
| 250 | 5.0273  | 2.9488  | 1.7955  | 1.3628  | 2.1598  | 3.8673  | 17.1615                  |
| 350 | 5.8293  | 3.6676  | 1.8670  | 1.4032  | 2.7535  | 5.3320  | 20.8527                  |

Table 4: Summary of average Nusselt numbers $\overline{Nu}$ for six blocks individually and in total for three Reynolds numbers at $Pr = 0.71$ in case of two partitions.

| Re  | Block 1 | Block 2 | Block 3 | Block 4 | Block 5 | Block 6 | $\overline{Nu}$ (total) |
|-----|---------|---------|---------|---------|---------|---------|--------------------------|
| 100 | 3.2791  | 1.8265  | 1.6086  | 1.8914  | 1.5810  | 1.7583  | 11.9449                  |
| 250 | 4.9303  | 2.2066  | 1.1352  | 2.5811  | 1.3338  | 2.4044  | 14.5915                  |
| 350 | 5.7620  | 2.4463  | 1.1924  | 2.9056  | 1.2632  | 2.7495  | 16.3191                  |

why $\overline{Nu}$ are 2.5811 and 2.9056 in terms of block 4 for Re = 250, 350. However, the change in the values of $\overline{Nu}$ repeats in terms of block 5. For Re = 100, patient at block 5 gets most air and that is also due to vorticity, which is seen in Figure 9. For two other Re, these recirculations appear over block 6, which also lead to an increase in $\overline{Nu}$ as per Table 4.

Comparing the results after analyzing Tables 2, 3, and 4, few statements can be made. Heat transfer rate is at its highest level when one partition is present. For example, when there is not any partition, total $\overline{Nu}$ is 15.8885 for Re = 250 and it rises to 17.1615 when one partition is present. However, placing two partitions create one extra obstacle for airflow and $\overline{Nu}$ decreases to 14.5915. Same variations can be observed for Re = 100 and Re = 350 as well.

The finding of three case studies can be related to the need of airflow of hospital patients. For instance, if a hospital ward does not have any obstacle or partition between any bed, patient who is in need of most airflow should be put on block (bed) 1. If anyone needs less air due to fever or is suffering from any type of airborne disease or germs, he or she should be kept at block 6 or on any bed which is farthest to the inlet.

Consequently, if the ward has one partition in the middle (which is pretty common in hospital nowadays), both blocks (beds) 1 and 2 will be just fine for more air. If disease is related to air, these two beds in particular should be avoided. For moderate airflow, any bed or block after the first two should be considered.

Last but not least, if three different zones are available in the ward due to two partitions, any bed between 3 and 6 should be okay for normal airflow. Blocks (beds) 1 and 2 should be kept for patients who are suffering from acute temperature related disease. By any chance, if none of those beds are available, block (bed) 4 will be a pretty good replacement.

6. Local Reynolds Number

Local Reynolds numbers ($Re_l$) for all obstacles have been computed at the mid of the gap between block and top wall for Case II (with one partition) at Re = 100. They are 61.54 for block 1, 35.34 for block 2, 25.54 for block 3, 36.93 for partition, 16.32 for block 4, 24.54 for block 5, and 32.19 for block 6. The above results demonstrate that as the air enters the domain and flows far away from the inlet, the inlet air velocity also reduces and, consequently, the local $Re_l$ values also decrease. Block 1 has the highest local $Re_l$ value since the inlet velocity is maximum at this position. After gradual decline of the numerals, block 4 has negative local $Re_l$ due to the negative velocity of the recirculation zone. The values then increase as the air flows up towards the outlet but cannot attain the maximum value due to the distance from the inlet.

7. Conclusion

In this paper, the study of airflow on mixed convection flow inside a hospital ward has been analyzed using the Lattice Boltzmann Method. The changes in the patterns of airflow have been observed in three different case studies. The
code validation has been carried out for three different Re and agreement has been shown as well. In the case studies, LBM was able to capture the convective structure as the air flowed over the room and even when the partition was present. It was found that the heat transfer process and flow characteristics depend on different Re. Moreover, the presence of the partition in each case was found to have significance on the pattern of airflow in both streamlines and isotherms on a particular Ri and Gr. Some conclusions are summarized as follows:

(a) A proper code validation with previous numerical investigations implies that Lattice Boltzmann Method is indeed an appropriate method for studying mixed convective airflow.

(b) Generally, the increase in Reynolds number resulted in augmentation of heat transfer. The pattern of airflow also changed.

(c) As the Reynolds number increases, the Mach number decreases. The Mach number cannot be more than 0.3 to satisfy the condition of flow in incompressible fluid.

(d) Since local Re is directly proportional to the velocity of inlet flow, therefore, as the air gradually flows away from the inlet, the flow velocity reduces for which local Re also decreases.

(e) Placing partition between the blocks or beds had effects on the airflow structure and for different cases, the results were different.

(f) The most effective rate of heat transfer was found when one partition was present, which were due to recirculations in the contours.

(g) Influence of two partitions on heat transfer was less for all three Reynolds numbers, which indicates that air did not get enough space to flow freely and that led to a fall in heat transfer rate.

(h) Patients who are in need of most air should be kept near the inlet and patients who do not need to be exposed directly to air should be moved near the outlet.

### Nomenclature

**English Symbols**

- a: Height of the partition
- b: Width of the partition
- c: Lattice speed
- \( \vec{v} \): Particle velocity
- F: External forces
- \( f \): Distribution function for velocity
- \( f^{eq} \): Equilibrium distribution function for velocity
- Gr: Grashof number
- \( g_{z} \): Gravitational acceleration in y-direction
- g: Distribution function for temperature
- \( g^{eq} \): Equilibrium distribution function for temperature
- H: Height of the hospital ward
- h: Height of each block
- k: Convective heat transfer coefficient of the flow
- L: Length of the hospital ward
- l: Length of each block
- Ma: Mach number
- N: Number of lattices parallel to y-direction
- Nu: Local Nusselt number
- Nu: Average Nusselt number
- n: Iteration index
- Pr: Prandtl number
- Re: Reynolds number
- Ri: Richardson number
- T: Temperature of the fluid
- \( T_{H}, T_{W} \): Hot wall temperature
- \( T_{C} \): Cold wall temperature
- t: Time
- \( \vec{u} \): Velocity vector
- u: Velocity component along x-direction
- v: Velocity component along y-direction
- \( U \): Bulk velocity
- \( w_{j} \): Weighted factor
- \( x, X \): Horizontal axial coordinate
- \( y, Y \): Vertical axial coordinate

**Greek Symbols**

- \( \alpha \): Thermal diffusivity
- \( \mu \): Dynamic viscosity of the fluid
- \( \nu \): Kinematic viscosity
- \( \rho \): Density
- \( \tau_{v} \): Single-relaxation time based on \( v \)
- \( \tau_{\alpha} \): Single-relaxation time based on \( \alpha \)
- \( \theta \): Nondimensional temperature
- \( \phi \): Generic variable
- \( f_{\Omega} \): Collision operator
- \( \nabla \): Gradient operator

### Competing Interests

The authors declare that they have no competing interests.

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