Current knowledge on the sensitivity of the $^{68}$Ga-somatostatin receptor positron emission tomography and the SUV$_{\text{max}}$ reference range for management of pancreatic neuroendocrine tumours

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Abstract Physiologically increased pancreatic uptake at the head/uncinate process is observed in more than one-third of patients after injection of one of the three $^{68}$Ga-labelled octreotide-based peptides used for somatostatin (sst) receptor (r) imaging. There are minor differences between these $^{68}$Ga-sstr-binding peptides in the imaging setting. On $^{68}$Ga-sstr-imaging the physiological uptake can be diffuse or focal and usually remains stable over time. Differences in the maximal standardised uptake values (SUV$_{\text{max}}$) reported for the normal pancreas as well as for pancreatic neuroendocrine tumour (PNET) lesions may be related to several factors, including (a) differences in the peptide binding affinities as well as differences in sstr subtype expression of pancreatic $\alpha$- and $\beta$-cells, and heterogeneity / density of tumour cells, (b) differences in scanner resolution, image reconstruction techniques and acquisition protocols, (c) mostly retrospective study designs, (d) mixed patient populations, or (e) interference with medications such as treatment with long-acting sst analogues. The major limitation in most of the studies lies in the lack of histopathological confirmation of abnormal findings. There is a significant overlap between the calculated SUV$_{\text{max}}$-values for physiological pancreas and PNET-lesions of the head/uncinate process that do not favour the use of quantitative parameters in the clinical setting. Anecdotal long-term follow-up studies have even indicated that increased uptake in the head/uncinate process still can turn out to be malignant over years of follow up. SUV$_{\text{max}}$-data for the pancreatic body and tail are limited. Therefore, any visible focal tracer uptake in the pancreas must be considered as suspicious for malignancy irrespective of quantitative parameters. In general, sstr-PET/CT has significant implications for the management of NET patients leading to a change in treatment decision in about one-third of patients. Therefore, follow-up with $^{68}$Ga-sstr-PET/CT is mandatory in the clinical setting if uptake in the head/uncinate process is observed.

Keywords $^{68}$Ga-somatostatin analogue · Neuroendocrine tumour · Pancreatic imaging · Uncinate process · Sensitivity · Specificity · SUV$_{\text{max}}$-calculation

Pancreas anatomy (Fig. 1) and surgery options (Fig. 2)

Removal of the primary tumour significantly prolongs survival of pancreatic neuroendocrine tumour (PNET) patients for both those with distant metastases and those without metastases. Therefore, early diagnosis/detection of PNETs is crucial for patient management. In general, surgery for PNETs is faced by two characteristic facts. On the one hand, preoperative diagnosis/localisation is challenging, and on the other hand, surgery of the pancreas can result in life-threatening complications. Once the diagnosis is established, choice for the optimal surgical procedure has to be made [1]. The criteria that influence this decision are the localisation of the PNET within the pancreas (caput, corpus, tail), type of PNET (i.e., insulinoma, gastrinoma, non-functioning tumours, multiple PNETs in multiple endocrine neoplasia (MEN) I syndrome), and localisation of the PNET in...
correlation to the pancreatic duct. Preservation of endocrine function, if at all possible, should be one consideration in the choice of operation. A radical resection should always be considered, at least for tumours of >2 cm even in cases of known distant metastases with impact on further prognosis [2]. A total of more than 60 % 5-year survival rates can be achieved after R 0-resection, independently of the extent of surgery with surgical mortality below 5 % and acceptable morbidity between 20 and 30 % in specialised centres [3]. For preoperative localisation of small PNET/duodenal wall $^{68}$Ga-somatostatin(sst)-receptor(r)-PET/CT showed high sensitivity for delineation of malignant lesions [4].

Pancreas imaging modalities

There are different metabolic imaging methods, various tracers, and several anatomic modalities to stage PNETs. In principle, morphologic techniques bear the risk of underestimation. $^{68}$Ga-sstr-PET/CT in combination with diffusion-weighted magnetic resonance imaging (DW-MRI) is currently the most promising technique for investigating NETs. The calculated sensitivity from pooled data of 52 studies was highest for sstr-PET compared to endoscopic or intraoperative ultrasound, sstr-scintigraphy, dual-phase (DP)-CT, DW-MRI, and $^{18}$F-FDG-PET, according to a recent extensive review by Bodei et al [5]. In a small number of patients, other molecular PET tracers such as $^{18}$F-DOPA, $^{11}$C-
5-HTP [6] or the $^{68}$Ga-exendin-4 targeting glucagon-like peptide-1 (GLP-1) [7] receptor tracer may locate a lesion when sstr-PET/CT is negative.

**Basis of pancreatic imaging with sstr-ligands**

**Expression of sstr subtypes on normal pancreatic and on pancreatic neuroendocrine tumour cells**

For PNETs peptide receptor imaging has been a challenge over the last 20 years, and still is. In principal, NET cells may express much higher amounts of sstr than normal tissue or blood cells providing the basis for imaging and treatment of sstr-positive tumour lesions. However, different primary tumours and metastases may express different amounts as well as different types of sstr-subtypes, and peptide ligands may bind differently to the five sstr-subtypes known [8, 9].

In fact, not too much is known about the normal in-vivo expression of sstr—and there may be large inter-individual variation as well. Physiologically, several normal organs show an increased sstr-expression. Therefore, different organs including the spleen, liver, pituitary, thyroid, kidneys, adrenal glands, salivary glands, and “the pancreas” may be visualised by $^{68}$Ga-sstr-PET-imaging.

Usually this physiologic pancreatic uptake appears as a “faint” uptake along the head, body, and tail of the pancreas that is believed to be a result of binding with high affinity to pancreatic islet cells that express various sstr subtypes. Pancreatic polypeptide (PP) cells are not distributed equally in the gland; they are the most abundant cell type in the posterior part of the pancreatic head whereas they are scarce or absent in the remainder of the gland. This lobe probably originates from the ventral pancreatic bud during embryogenesis [10]. Variability in the normal expression of sstr1-5 subtypes among the different human endocrine pancreatic cells was shown by Portela-Gomes et al [11]. Sstr generally exerts inhibitory effects on hormone release produced in the pancreatic islets [12] mediated through the five known G protein-coupled sstr subtypes [13].

**Sstr binding affinity of $^{68}$Ga-sstr-ligands**

Different sst-analogues have been introduced for $^{68}$Ga-sstr-PET-imaging over the past 10 years, with the first PET-imaging studies in humans performed with $^{68}$Ga-1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid (DOTA)-Tyr3-octreotide (TOC) [14]. The small structural change achieved by introducing the metal gallium instead of other trivalent metals (indium, yttrium, lutetium) appeared to impact the affinity profile for the different sstr-subtypes (Table 1, [15–18]). Furthermore, the pharmacokinetic properties also showed improvement [15]. The Ga-complexes of sst-analogues commonly show a higher binding affinity for sstr2 when compared with the corresponding complexes with indium, yttrium, or lutetium. The increased hydrophilicity of the Ga-complex furthermore results in an increased renal elimination. Together with an improved accumulation of $^{68}$Ga-DOTA-TOC in the tumour lesions these pharmacokinetic properties lead to a high lesion contrast within a short time interval post injection, which is of particular importance considering the short half-life of $^{68}$Ga (68 min). Ga-DOTA-Tyr3-octreotate (TATE) with a C-terminal threonine instead of the corresponding amino alcohol in DOTA-TOC shows a 10-fold higher affinity towards sstr2, whereas the affinity to sstr3 and sstr5 is reduced and the affinity to sstr4 is increased when compared with Ga-DOTA-TOC. Ga-DOTA-1-Nal3-octreotide (NOC) with tyrosine in position 3 replaced for 1-naphthyl-alanine shows a similar sstr2-binding affinity together with a more than 10-fold increased affinity for sstr3 and sstr5 in comparison to Ga-DOTA-TOC and a similar affinity to sstr4 when compared to Ga-DOTA-TATE [16].

| Peptide     | sstr1 | sstr2 | sstr3   | sstr4   | sstr5   |
|-------------|-------|-------|---------|---------|---------|
| DOTATOC     | >10,000 | 14±2.6 | 880±324 | >1,000  | 393±84  |
| DOTATATE    | >10,000 | 15±0.4 | >1,000  | 453±176 | 547±160 |
| DOTALAN     | >10,000 | 26±3.4 | 771±229 | >10,000 | 73±12   |
| Ga-DOTATOC  | >10,000 | 2.5±0.5 | 613±140 | >1,000  | 73±21   |
| Ga-DOTATATE | >10,000 | 0.2±0.04 | >1,000  | 300±140 | 377±18  |
| Ga-DOTANOC  | >10,000 | 1.9±0.4 | 40.0±5.8 | 260±74  | 7.2±1.6 |
| Y-DOTATOC   | >10,000 | 11±1.7 | 389±135 | >10,000 | 114±29  |
| Y-DOTATATE  | >10,000 | 1.6±0.4 | >1,000  | 523±239 | 187±50  |
| Y-DOTANOC   | >1,000  | 3.3±0.2 | 26±1.9  | >1,000  | 10.4±1.6 |
| Y-DOTALAN   | >10,000 | 22.8±4.9 | 290±105 | >10,000 | 16.3±3.4 |

The table lists the values for the inhibitory constant (nmol/L) for sstr-binding peptides and their gallium and yttrium complexes. The IC$_{50}$-value indicates the concentration when 50% of binding is inhibited.
Pancreatic sstr-imaging—sensitivity, specificity, and SUV\textsubscript{max} (Table 2)

Sstr-PET is nowadays the established standard method for molecular imaging of NET. A detailed procedure guideline for PET/CT with \textsuperscript{68}Ga-sst-analogue imaging was summarised by the Oncology Committee of the EANM [19]. This (early) guideline already mentions that physiological focal tracer uptake may mimic tumour disease in the pancreas, most frequently in the head/uncinate process, and also strongly recommends anatomical localisation with other imaging modalities.

Here, we overview the currently available data on the diagnostic performance of \textsuperscript{68}Ga-sstr-PET in the detection of PNETs. We understand that patients at various centres occasionally have undergone surgery for suspected PNETs visualised by sst analogs in which no tumours were ultimately identified by pathohistology.

Data for \textsuperscript{68}Ga-DOTA-TOC-PET

In the first prospective publication [20] in 84 patients with known or suspected NET we described an increased uptake in the pancreatic head in 57 (67.8 \%) / 84 patients, but we did not quantify the uptake in terms of SUV\textsubscript{max}. The criteria for visual study interpretation involved a malignant pancreatic head: an irregular or protrusive shape of finding and clear delineation from adjacent tissue with higher uptake than the liver. By these criteria, PET identified 23 findings in the pancreas while there were only 21 identified with SPECT and 19 with CT. Only one false positive (FP) finding with an enhanced tracer uptake in the pancreatic head was found in a patient who had clinical symptoms in terms of persistent diarrhoea suggestive for a PNET (Fig. 3).

One of the first papers on SUV\textsubscript{max}-calculation [21] indicated that individual sstr-mediated tumour uptake shows a large range of variation. In this retrospective study the SUV\textsubscript{max} values for tumours were ranging between 6.4 and 267, but not all tumours of this study were NETs. The study was aimed at evaluating if calculation would predict a response to peptide receptor radionuclide therapy (PRRT). In seven patients, malignant lesions of the pancreas were used for assessment of treatment response. These seven patients showed high SUV\textsubscript{max} values upon the initial visit (mean 43.6; range 20.5–94). Although the reference standard (clinical follow-up by CT or MRI) indicated progressive disease (PD) in four patients and stable disease (SD) in three patients, a significant decline of overall SUV\textsubscript{max} values was observed with regard to the pancreatic lesion (mean 28.9; range 18–28.9) after finalisation of PRRT. It is open for discussion as to whether the decline of tracer uptake despite PD presents a partial therapy success in terms of mixed response or whether it indicates a further step towards dedifferentiation at a cellular level.

In order to evaluate and establish the \textsuperscript{68}Ga-DOTA-TOC uptake for PNET lesions and differentiate the physiologic pancreatic uptake, our group calculated the SUV\textsubscript{max} [22]. The SUV\textsubscript{max} amounted to 34.6 ± 17.1 for PNET lesions (n = 43). We differentiated these lesions and calculated 33.6 ± 14.3 for tumours of the uncinate process (n = 30) and 36.3 ± 21.5 for the pancreatic tail (n = 13). The pancreatic body served as “normal pancreas” for calculating the ratios. “Normal” pancreas was defined as faint/no uptake. Finally, a mean cut-off SUV\textsubscript{max}-value of 17.1 was assessed for differentiating tumours in the uncinate process with a specificity of 93.6 \% and a sensitivity of 90 \%. At this cut-off value we found true positive (TP) = 27, FP = 20, false negative (FN) = 3, true negative (TN) = 290, and the three cases of FN (i.e., CT-positive) with SUV\textsubscript{max}-values of 14.7, 12.8, and 11.7. We concluded that physiological uptake can pose difficulties in correctly analysing this region. In our cohort of >1500 \textsuperscript{68}Ga-DOTA-TOC-PET/CT scans (years 2010–2014), 115 studies were performed to detect or exclude pancreatic malignancy (unpublished data); for 14 patients who underwent subsequent surgery, the SUV\textsubscript{max}-data of histopathologically verified PNETs indicated large variation, for the uncinate process 33.2 ± 15.1 (n = 3), pancreatic body 57.9 ± 67.6 (n = 3), and the pancreatic tail 47.2 ± 39.7 (n = 9). Cut-offs obtained by ROC (Receiver Operating Characteristic) analyses were 17.1 for the uncinate process (specificity 92 \%; sensitivity 100 \%), for the pancreatic body 14.4 (specificity 100 \%; sensitivity 100 \%) and for the pancreatic tail 12.0 (specificity 92.5; sensitivity 88.9 \%).

Al-Ibraheem et al. [23], reported no visual uptake in the pancreatic head in 20 of 43 (46.6 \%) consecutive patients. In the other 23 patients (53.4 \%) either focal uptake (n = 10) or an irregular uptake pattern (n = 13) were observed. The SUV\textsubscript{max} for the 20 patients without visual uptake amounted to 4.0 ± 0.8 (range 2.4 to 5.3). For another 20 patients with noticeable uptake without malignancy (eight patients with focal uptake, 12 patients with irregular uptake) the SUV\textsubscript{max} amounted to 9.3 ± 3.1 (range 5.1 to 15.5). In subsequent studies, malignancy could only be histologically proven in three patients (two with focal and one with irregular uptake) and the SUV\textsubscript{max} in these patients amounted to 51.6 ± 15.7 (range 34.1 to 64.2). The authors concluded that if the uptake in the pancreatic head is similar to the uptake in the liver, then a physiological condition is most likely, but also noted that misalignment due to respiratory motion must always be taken into account.

Kumar et al. [24] found 100 \% sensitivity for detecting primary pancreatic tumours as well as metastatic disease and reported that the detection rate of PET/CT was higher compared to CT alone, both for primary tumours (20 versus 15) as well as metastases (13 versus seven). They reported no significant correlation of SUV\textsubscript{max}-values with tumour size. Primary tumours were localised in the pancreatic head in seven, in the body in nine and in the tail in three patients. Median SUV\textsubscript{max}
| Radiopharmaceutical | Authors (Ref.) | Design | No of pts. | Quantitative parameters (SUV<sub>max</sub>) | Diagnostic performance (Sens./Specif.) | “Gold”/Reference standard |
|---------------------|---------------|--------|------------|------------------------------------------|--------------------------------------|--------------------------|
| ⁶⁸Ga-DOTA-TOC       | Gabriel et al. (20) | Prospective | 84 | Not done | Sensitivity 100 %, Specificity 88.8 %* | Follow-up/Histopathology |
|                     | Gabriel et al. (21) | Retrospective | 46 | Mean 43.6 (range 20.5–94) | Not done | Follow-up |
|                     | Kroiss et al. (22) | Retrospective | 249 | Cut-off 17.1 (malignant/non-malignant) 311 | Sensitivity 90 %, Specificity 93.6 % | Follow-up |
|                     | Al-Ibraheem et al. (23) | Retrospective | 43 | Mean 33.6 ± 14.3 PNET uncinate process 311 | Not done | Follow-up |
|                     | Kumar et al. (24) | Retrospective | 20 | Median 12.6 (range 8.8–27.6) | Sensitivity 100 % | Follow-up/Histopathology |
|                     | Jacobsson et al. (25) | Retrospective | 50 | Mean 18.6 ± 9.8 (range 7.8–34.8) previously unknown PNET | Not done | Concomitant CT |
| ⁶⁸Ga-DOTA-NOC       | Prasad V, Baum RP (26) | Retrospective | 50 | Mean 5.8 ± 2.0 (range 4–9.7) non-malignant 26 | Not done | Follow-up |
|                     | Castellucci et al. (27) | Retrospective | 100 | Mean 12.6 ± 2.2 non-malignant | Not done | Follow-up |
|                     | Prasad et al. (28) | Retrospective | 59 | Mean 18.6 ± 9.8 (range 7.8–34.8) previously unknown PNET | Not done | Follow-up |
|                     | Krausz et al. (29) | Retrospective | 96 | Mean 25.7 ± 28.8 (range 5.5–165) PNET | Not done | Follow-up |
|                     | Sharma et al. (30) | Retrospective | 35 | Mean 26.1 ± 14.5 (range 8.7–42.4) previously known PNET | Not done | Follow-up |
| ⁶⁸Ga-DOTA-TATE       | Wild et al. (31) | Retrospective | 8 | Mean 14.7 ± 6 (range 3–32.5) | Sensitivity 85.7 %, Specificity 79.1 % | Follow-up/Histopathology |
|                     | Skoura et al. (32) | Retrospective | 728 | Mean 9.2 ± 2.9 (without pathology) | Not done | Follow-up/Histopathology |
|                     | Kunikowska et al. (33) | Retrospective | 250 | Mean 9.2 ± 3.3 without pathology in 41/250 pts (16.4 %) | Not done | Follow-up/Histopathology |
|                     | Haug et al. (34) | Retrospective | 104 | Mean 26.16 ± 27.38 (range 6.2 to 120) | Not done | Histopathology |
|                     | Schmid-Tannwald et al. (35) | Retrospective | 18 | Sensitivity 100 %, Specificity 80 % | Follow-up/Histopathology |
|                     | Etchebehere et al. (36) | Prospective | 19 | Not done | Follow-up/Histopathology |

*with regard to patients with suspected NETs
²14 FP in 1258 scans, 4 of them for the pancreas
³7 FP and 7 FN, sites of findings not indicated
of primary tumours amounted to 12.6 (range 8.8 to 27.6), similar to the values reported by Prasad and Baum [25] for ⁶⁸Ga-DOTA-NOC. In Fig. 2 they show a case of significant uptake in the pancreatic head/uncinate. The authors state that there was no FP for primary PNETs and that all tumours were seen on ⁶⁸Ga-DOTA-TOC-PET.

Jacobsson et al. [26] retrospectively analysed their cohort and reported physiological ⁶⁸Ga-DOTA-TOC-uptake in the uncinate process in 35/50 (70 %) patients. These authors calculated a mean SUV<sub>max</sub> of 9.2±2.9 for the uncinate process using an isoactivity cut-off of >75 % and >50 % that equated to 7.8 and 6.0, respectively. The uncinate process activity versus pancreas body and tail varied between 3.0 and 4.3.

Prasad and Baum [25] reported an SUV<sub>max</sub>-value of 5.8±2.0 (range 4–9.7) for the physiological uptake of the uncinate process (n = 50) and significantly higher SUV<sub>max</sub>-values for PNETs (20.8±10.8; n = 26), providing high target to non-target ratios. The authors suggested that the uncinate process can be differentiated from pancreatic tumours with high diagnostic accuracy at an SUV<sub>max</sub>-cut-off of 8.6 (sensitivity 92 %, specificity 94 %).

Castellucci et al. [27] retrospectively assessed 100 patients and identified 23 % diffuse and 8 % focally increased pancreatic tracer uptake in patients with extra-pancreatic NETs in whom follow-up PET indicated no change of SUV<sub>max</sub>-values over time, thus suggesting no disease. The SUV<sub>max</sub> was 12.6.
±2.2 for those with focal uptake and 5.0±1.6 for diffuse uptake. The values refer to uptake in the head/uncinate process without known pathology albeit no histology was obtained. The authors state that the pancreatic pattern of uptake remained unchanged, regardless of whether it was focal, diffuse, or absent. They could not confirm the low cut-off value suggested by the Bad Berka group [20] or come close to our Innsbruck suggestion that the mean $SUV_{\text{max}}$-cut-off between benign and malignant pancreatic tissues should lie somewhat “higher”.

However, in a bi-centric study [28] in 59 NET-patients with unknown primary PNETs, PET/CT were able to localise the tumours in 35/59 (59 %) patients, including 16 patients with PNETs (five head, four body, three tail, three multifocal, and one unincute process). Notably, primary PNETs found on CT after retrospective analyses were reported in 8/16 patients (50 %)! The mean $SUV_{\text{max}}$ of previously identified unknown primary PNETs was 18.6±9.8 (range 7.8–34.8) and the mean $SUV_{\text{max}}$ in patients with a previously known PNET was 26.1±14.5 (range 8.7–42.4), suggesting that patients with known primary PNETs have higher sstr expression. Notably, the authors present a case of multifocal PNET in Fig. 2a of their study that was only detected by PET/CT at the pancreatic tail but was missed by endoscopic ultrasound (EUS). Furthermore, the average time interval between the first biopsy-proven diagnoses of NET and the first evidence of a primary tumour on PET/CT was found to be approximately 29 months!

Krausz et al. [29] reported for 35 PNETs an $SUV_{\text{max}}$ ranging between 5.5 and 165 (mean 25.7±28.8). Among 63 cases without previously known pathology, uptake was suspicious for tumour in 24 cases with an $SUV_{\text{max}}$ ranging between 4.7 and 35 (mean 16.3±8.0). In 38 sites they judged this uptake as physiological, generally lower relative to adjacent structures ($SUV_{\text{max}}$ 2.2–12.6; mean: 6.6±2.2). In 24 scans with suspected tumour and in 37/38 scans with physiological uptake, diagnostic CT/MRI/EUS failed to detect tumour, suggesting that these investigations do not significantly add to a diagnosis if uptake is observed in the pancreatic uncinate. No ROC analysis is available because of low specificity and sensitivity rates.

Sharma et al. [30] reported a mean overall $SUV_{\text{max}}$ for primary PNETs of 14.7±6 (range 5–32.5), which was significantly higher than that of metastases overall ($P=0.001$), as well as in the diagnosis/staging ($P=0.041$) and restaging ($P=0.0003$) subgroups. For the staging/diagnosis group ($n=88$), the overall sensitivity was 73 %, specificity was 50 %, and accuracy was 70.4 %, and these values were significantly lower ($p<0.0001$) when compared to the restaging group (98.6, 100, 98.8 %, respectively). Of the 88 studies, 57 were TP, five were TN, five were FP and 21 were FN, and of the latter ones most of these were known or suspected insulinomas. In the non-insulinoma group the sensitivity was 100 %, specificity was 57.1 %, and accuracy was 94.8 %.

### Data for $^{68}$Ga-DOTA-TATE-PET

Poeppel et al. [31] reported in 40 patients (head-to-head comparison) with metastasised NETs that significantly fewer lesions were detected by $^{68}$Ga-DOTA-TATE as compared to $^{68}$Ga-DOTA-TOC ($p<0.05$, 254 vs. 262 lesions), but no overall difference was found for detection of regions (78 vs. 79 regions were positive). However, the $SUV_{\text{max}}$-values were significantly lower for $^{68}$Ga-DOTA-TATE compared to $^{68}$Ga-DOTA-TOC ($p<0.01$; 16.0±10.08 vs. 20.4±15.7) across all lesions including those of the pancreas.

In contrast, Kabasakal et al. [32] reported in a head-to-head comparative study a comparable diagnostic accuracy for both sstr peptides in 20 tumour patients on a visual scale. However, $^{68}$Ga-DOTA-TATE identified 14 more tumour lesions because of superior uptake compared to $^{68}$Ga-DOTA-TOC. In fact, the $SUV_{\text{max}}$-values calculated for the lesions were significantly higher, with 29.9±26.4 for $^{68}$Ga-DOTA-TATE compared to 24.5±20.3 for $^{68}$Ga-DOTA-TOC ($p<0.001$). Pancreatic uptake was not further classified in this paper.

A prospective study from London [33] performed in 18 patients reported a lesion-based overall sensitivity of 93.5 % for $^{68}$Ga-DOTA-TOC compared to 85.5 % for $^{68}$Ga-DOTA-TATE, which was due to a significantly ($p<0.001$) higher detection of liver metastases. As for PNETs, $^{68}$Ga-DOTA-TOC detected 7/8 whereas $^{68}$Ga-DOTA-TATE detected only 3/8 lesions. In two patients with MEN 1 $^{68}$Ga-DOTA-TATE detected only one PNET whereas $^{68}$Ga-DOTA-TOC detected multiple PNETs. Both tracers detected an uncinate process lesion in two patients that were not confirmed by cross-sectional and follow-up imaging and were therefore regarded as FP. The $SUV_{\text{max}}$-values for the physiological pancreas were significantly ($p<0.001$) higher for $^{68}$Ga-DOTA-TATE as compared to $^{68}$Ga-DOTA-TOC (3.5, 3.0–4.3 vs. 2.5, 2.0–3.4). The same group also reviewed their cohort of 728 patients and found 14 FP scans out of 1258, four of them for the pancreas, with an overall sensitivity of 97 % and specificity of 95.1 %, and change in treatment management in 41 % of patients owing mainly to new unexpected findings [34].

In a retrospective evaluation Hofman et al. [35] communicated a high impact on patient management, including curative surgery, by identifying a primary site and directing patients with multiple metastases to systemic therapy. Uncinate process uptake was generally not seen on $^{111}$In-octreotide imaging but was visualised in 32 % ($n=19$) by PET. One FP case was due to moderately increased uptake in the uncinate process that appeared particularly prominent. This case was concordant with a previous $^{111}$In-octreotide scan and was performed to exclude additional disease. The patient underwent surgery and histology revealed no evidence of a NET, although the referer marked that the patient’s symptoms and biochemistry improved. They also demonstrate the case of a previously unknown PNET in Fig. 4.
Kunikowska et al. [36] reported increased physiological uptake in the uncinate process in 41/250 patients (16.4%) with an SUV max of 9.2 ± 3.3. In this study, sites of physiological focal uptake were confirmed to be disease-free in subsequent follow-up imaging studies as well as in clinical follow-up. The authors also reported in one patient a 1-cm lesion that was only detected by DW-MRI, and subsequent surgical resection revealed an adenocarcinoma with hyperplasia of neuroendocrine cells (Fig. 8 of their paper, SUV max 7.2; personal communication).

Haug et al. [37] indicated a sensitivity of 81% and a specificity of 90%, resulting in an accuracy of 87% with seven FN and seven other FP cases in suspected NETs. They also reported a change in surgical management in 9/44 (20%) of patients; among those were 6/18 (33%) patients with PNETs [38].

Schmid-Tannwald et al. [39] showed that 68Ga-DOTA-TATE-PET/CT is more sensitive than DW-MRI in the detection of PNETs in 18 patients in the first direct head-to-head comparative study of patients with histologically proven well-differentiated or intermediate PNETs. The cohort comprised five lesions in the head, three in the uncinate process, six in the body and nine in the tail. In this study, the SUV max for the PNETs were 36.46 ± 27.38, range 6.2–120. In Fig. 4 they show the case of a patient with PNET that could neither be visualised by DW-MRI nor CT. Only the fused PET/CT image made the lesion clearly identifiable by its increased uptake of 68Ga-DOTA-TATE.

Similarly, Etchebehere et al. [40] reported for 19 patients a higher sensitivity of PET/CT over DW-MRI (1.5 T) and SPECT/CT (99mTc-6-hydrazinonicotinic acid (HYNIC)-octreotide). This study was performed prospectively and included a biopsy of suggestive lesions. For the pancreas, PET/CT detected more lesions versus SPECT/CT (P = 0.0455) and WB-DWI (p < 0.0455) including a case of unknown primary in the pancreas uncinate (sensitivity 100%, specificity 80%, accuracy 84%), but also reported on one FP-uptake in the process uncinate. Notably, in Fig. 1 the authors demonstrate the case of an unknown primary which was clearly marked only on 68Ga-DOTA-TATE-PET/CT while neither SPECT/CT nor MRI identified the tumour. Only retrospective analysis detected the primary (0.4 cm lesion) on dedicated CT performed 4 years previously!

**Data for other sstr-binding radiopharmaceuticals**

**68Ga-DOTA- lanreotide (LAN) and 64Cu-DOTA-TATE-PET**

The only PNET imaged by 68Ga-DOTA-LAN, which was negative by 68Ga-DOTA-TOC, exhibited an SUV max of 6.5 [41]. Pfeifer et al. [42] reported a case of previously unknown PNET that was only confirmed 6 months later on CT in a patient with MEN I syndrome.

**Accuracy of SUV max-determination and limitation**

Sstr targeting is demonstrated by visualisation of tumour lesions. This visualisation is based on an increased expression of sstr by tumour lesions [8, 9]. There is a “visual scale” introduced initially by the group of Krenning et al. [43], but several other groups have also tried to quantify the sst tracer uptake. This can be (semi) quantified by SUV max or dosimetry calculation and qualifies a patient as being sstr-positive on a scan with potential for PRRT [44]. Several factors may interfere with SUV max-calculation.
Sstr-binding affinity

The discussion was raised that the (slightly) different sstr2-binding affinities for $^{68}$Ga-DOTA-TOC, $^{68}$Ga-DOTA-NOC, and $^{68}$Ga-DOTA-TATE may result in a somewhat different SUV$_{\text{max}}$ for tumours and probably also for the physiological uptake. Direct comparative head-to-head PET/CT data were published only in few numbers of patients [31–33]. Due to the 10-fold higher binding affinity for the sstr2 subtype, DOTA-TATE may theoretically bear the potential for better tumour detection. Interestingly, the comparative study of $^{68}$Ga-DOTA-TOC and $^{68}$Ga-DOTA-TATE exhibited a higher tumour uptake for $^{68}$Ga-DOTA-TOC [31]. The higher affinity of $^{68}$Ga-DOTA-TATE to sstr2 could be contra-balanced by the higher affinity of $^{68}$Ga-DOTA-TOC to sstr5. The two radioligands showed, however, a high inter- and intra-patient variability and possessed a comparable diagnostic value for the detection of NET lesions. Potential advantages of $^{68}$Ga-DOTA-TOC are the superior SUV$_{\text{max}}$ derived for tumour lesions and the higher tumour-to-kidney ratio. For $^{68}$Ga-DOTA-NOC a better visualisation of normal organs, especially the spleen, was reported because of the broader subtype affinity profile [45]. $^{68}$Ga-DOTA-NOC showed a lower normal liver and pancreas uptake with respect to $^{68}$Ga-DOTA-TATE, allowing for a higher detection rate of liver metastases and PNETs. On the other hand, $^{68}$Ga-DOTA-TATE showed a higher uptake in organs with predominant sstr2 expression and in bone metastases than $^{68}$Ga-DOTA-NOC. $^{68}$Ga-DOTA-NOC PET was shown to be superior in the detection of PNETs, however, with both tracers FP results for the pancreatic uncinate were reported [33]. Similar FP findings have been reported for $^{68}$Ga-DOTA-TOC and $^{68}$Ga-DOTA-NOC by others [22, 27].

Uptake in normal pancreas is thought to be based on the presence of sstr on the islet cells [46]. High concentration of sstr2 has been consistently found on pancreatic α- and β-cells but sstr3 and sstr5 concentration is still controversial. This normal expression may increase the risk of FP findings. However, Wittingen and Frey [47] demonstrated that the islet concentration in the tail is greater as compared with the uncinate head/body, which does not support this hypothesis. The controversial expression of sstr may be one reason for the considerable overlap of the values reported in the literature, though physiological uptake in the pancreas was generally associated with lower SUV$_{\text{max}}$-values compared to tumour lesions. Furthermore, the calculated SUV$_{\text{max}}$-values for PNETs may have a broad range of variation as indicated in Table 2. Whereas Miederer et al. [48] found a positive correlation of SUV$_{\text{max}}$ with the sstr2 expression using $^{68}$Ga-DOTA-TOC-PET/CT, there is some evidence that at an SUV$_{\text{max}}$ greater than 25 the calculation may not reflect solely sstr expression of tumours [49].

Scanner resolution and image reconstruction techniques

The tomographic resolution of a PET scanner and the method of data reconstruction significantly affect SUV$_{\text{max}}$-calculation, especially for small NET lesions with high uptake. In a comparison of standardised protocols with 23 dedicated PET scanners Geworski et al. [50] demonstrated errors of up to 10 % in SUV$_{\text{max}}$-values. Furthermore, many centres were not able to maintain accurate SUV$_{\text{max}}$-calibrations without additional supervision, which can be another hindrance of reasonable SUV$_{\text{max}}$-calculation [51].

Time of flight (TOF) is a valuable method for acquiring the signal-to-noise ratio [52]. Basically, TOF generates an increase in SUV$_{\text{max}}$. Therefore, the use of TOF has to be taken into account when comparing SUV values.

In recent years new reconstruction algorithms have continuously been developed that mainly confirm under the notation “resolution recovery”. These improving algorithms take known scanner, bed, and physical geometries into account and vary from vendor to vendor. On the one hand they may enhance the signal-to-contrast ratios, and on the other hand, they may also reduce the activity administered to the patient or reduce the time per bed position. The common hurdles to introducing these patient exposure-reducing and image-improving algorithms quickly into daily routine are the significant costs, the need for physician training and familiarity with modified images, and the strongly reduced possibility to use the different reconstructed images for follow-up comparison. Therefore, the PET scanner scene is very heterogenic in terms of technological standard (e.g., TOF or nonTOF) and the use of modern reconstruction algorithms. This makes it almost unreliable in comparison of SUV$_{\text{max}}$-values from sites with different scanners.

The Innsbruck data with $^{68}$Ga-DOTA-TOC [22] were derived with the use of TOF and geometric modelling (VuePoint FX, GE®), contrary to the reconstruction methods used in the studies reported by Prasad and Baum [25] with $^{68}$Ga-DOTA-NOC and Pöppel et al. [31] with $^{68}$Ga-DOTA-TATE.

Other factors

Tracer uptake time

The initial patient study [20] clearly demonstrated that serial acquisition at different time points (20, 60, and 100 min p.i.) provide different results with regard to image quality and count ratios. Based on the pharmacokinetics on one hand and on the rapid isotope decay on the other, the optimal time point for scanning should be 100 min p.i.. However, time points for scanning are still not standardized [43], but would be an important methodological requirement for comparison of semi-quantitative parameters.
Peptide mass

Some evidence suggests that the peptide mass may potentially influence the in-vivo binding and subsequently $SUV_{\text{max}}$ [53], but there exist no further data on this hypothesis.

Motion

Difficulties in image interpretation may also stem from respiratory motion contributing to FP pancreatic uptake. Therefore, attenuation correction is essential [54].

Influence of PRRT and other therapies

Receptor downregulation may become a problem under different therapy modalities and may also change receptor density due to dedifferentiation in the course of disease [45].

Impact for patient management

PNETs can present with various symptoms and clinical outcomes. Symptomatic tumours include insulinomas, gastrinomas, glucagonomas, VIPomas, and somatostatinomas, but most of the PNETs are non-functioning and present fairly late, usually with liver metastases. Thus, early and accurate localisation of primary tumours and metastases is essential for further patient management.

Hyperplastic changes of the NET cell may have the potential to evolve into neoplastic disease. This is particularly the case in the setting of MEN syndromes. Pseudohyperplasia of islet cells of the pancreatic head, however, is believed to be an age-dependent condition that differs from hyperplastic neoplastic NET disease [55]. The pancreas of patients with MEN1 (Fig. 2) typically contains multiple small NET-microadenomas [56]. It is supposed that the allelic loss of 11q13 in an islet cell sets the stage of NET development [57].

To our knowledge, no prospective study has so far specifically addressed the diagnostic performance with regard to the pancreas. The only information about the diagnostic performance of PET/CT has been derived from several retrospective studies using different sstr-avid tracers and protocols presented herein. Therefore, a standardised protocol is not yet available that especially addresses the knowledge about specificity of the technique. Are “FP findings” real non-tumour foci in PET/CT? What is the gold standard in this situation? Surgery? Follow-up? The uncertainty of this issue may also result in a patient tragedy [58].

Besides visual criteria to define abnormalities, the most attractive way to differentiate normal and abnormal pancreatic uptake might be based on quantitative parameters, in particular $SUV_{\text{max}}$-values. However, the retrospective analyses show some discrepancies with regard to this parameter. For instance, we [22] found an $SUV_{\text{max}}$ of 17.1 for $^{68}$Ga-DOTA-TOC that was best suited to discriminate between malignant and non-malignant lesions irrespective of the lesion diameter using ROC curves, while several other groups proposed somewhat different cut-off values. Extrapolating the data from the studies, the $SUV_{\text{max}}$ cut-off for $^{68}$Ga-DOTA-TATE should be around 20 and for $^{68}$Ga-DOTA-NOC more than 20 [31–33]. While we initially could not demonstrate a relevant clinical value of $SUV_{\text{max}}$ changes derived from $^{68}$Ga-DOTA-TOC studies in patients treated by PRRT [21], in a more recent publication Ambrosini et al. [59] recently demonstrated for $^{68}$Ga-DOTA-NOC that $SUV_{\text{max}}$ is a relevant prognostic factor in G1- and G2-PNETs. In their retrospective analysis they showed for 43 patients that at the 24-month follow-up the $SUV_{\text{max}}$ was significantly ($P=0.003$) higher for patients with SD than for those with PD, reporting an $SUV_{\text{max}}$ cut-off of 38.

However, some anecdotal examples show that even high $SUV_{\text{max}}$ values can be found during repeated investigations without clinical evidence of tumour development, such as those shown here in Fig. 3. Therefore, cut-off values should be cautiously considered in the decision to perform surgery or not, and to specifically guide the patient management.

Summing up all available data, $^{68}$Ga-sstr-PET/CT imaging is feasible to rule out well-differentiated PNET in most cases with high reliability, which can be helpful in patients where the primary NET site is supposed in the pancreas. On the other hand, some papers report on the potential value of $SUV_{\text{max}}$ calculation to assess NET tissue, however, this approach suffers from limitations mostly related to technical/methological shortcomings and sometimes the slow evolution of well-differentiated NETs. Therefore, prospective studies are required to standardise the procedure. Despite the frequent finding of enhanced uptake in the pancreatic head/uncinate process one should be cautious to assume this finding as normal to neglect the origin over time. In this situation at least another cross-sectional imaging modality, preferably DW-MRI, should be conducted to rule out any irregularity of the organ. Finally, it was already demonstrated that it is still possible that with a longer follow-up period some of the suggested foci that were “suspected tumours” and could not be verified by CT/MRI/EUS may be found to contain tumours in the future, such as recently demonstrated by Prasad et al. [28] or Etchebehere et al [40].

Conclusion

On the basis of the present data, the diagnostic algorithm is to perform a $^{68}$Ga-sstr-PET/CT study on initial staging of the NET patient since it is superior to sstr-SPECT/CT as well as to DW-MRI. With regard to the pancreas, however, the definitive accuracy has yet to be defined. A huge scale of results
can be observed to discriminate tumour from non-tumour findings by visual and in particular by quantitative scoring, from which it is not possible to make definite recommendations. The major limitation in most of these (single-centre) studies lies in the lack of histopathological confirmation of abnormal findings and the retrospective design. It must be mentioned that it is usually not feasible to obtain histopathological verification due to ethical and practical reasons, and therefore most of the published studies employed a combination of clinical and/or imaging follow-up.

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Compliance with ethical standards

Conflicts of interest The authors declare that they have no conflicts of interest.

Ethical approval Informed consent was obtained from all individual patients undergoing PET scans at the Medical University of Innsbruck. All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards.

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