In vivo measurement of cytoplasmic organelle water fraction using diffusion-weighted imaging: Application in the malignant grading and differential diagnosis of gliomas

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Abstract
Recently, we have proposed a theoretical modified tri-exponential model for multi-b-value diffusion-weighted imaging (DWI) to measure the cytoplasmic organelle water fraction (COWF). This study aims to investigate whether COWF maps are effective in evaluating the malignant degree of gliomas and distinguishing primary central nervous system lymphomas (PCNSL) from gliomas. We performed this retrospective study based on our prospectively collected data. All patients underwent preoperative multi-b-value DWI. Parametric maps were derived from multi-b-value DWI maps using the modified tri-exponential model. Receiver operating characteristic analyses were used to assess the diagnostic accuracy of the parameter maps. Pearson correlation coefficients were calculated to investigate the correlations between the parameters and the Ki-67 proliferation index.

A total of 66 patients were enrolled, including 16 low-grade gliomas (LGG), 45 high-grade gliomas (HGG), and 5 PCNSL. The mean COWF values were significantly different among LGG (3.1 ± 1.4%), HGG (6.9 ± 2.8%), and PCNSL (14.0 ± 2.2%) (P < .001). The areas under the curves of the mean COWF value in distinguishing HGG from LGG and distinguishing PCNSL from gliomas were 0.899 and 0.980, respectively. The mean COWF value had a moderate correlation with the Ki-67 proliferation index (r = 0.647).

The COWF map is useful in malignant grading of gliomas, and may be helpful in distinguishing PCNSL from gliomas.

Abbreviations: AUC = area under the curve, COWF = cytoplasmic organelle water fraction, DWI = diffusion-weighted imaging, HGG = high-grade gliomas, LGG = low-grade gliomas, PCNSL = primary central nervous system lymphomas, ROC = receiver operating characteristic, ROI = regions of interest.

Keywords: diffusion magnetic resonance imaging, glioma, Ki-67 antigen, lymphoma, neoplasm grading

1. Introduction
Glioma is the most common malignant brain tumor.1 It is of clinical need to classify the grade of gliomas as various stages of gliomas need different therapies. Traditionally, histopathologic examination is the gold standard for grading gliomas. However, high-grade gliomas (HGG) always contain both low- and high-grade components, leading to sampling error in pathological assessment.2,3 Besides, pathological grading can only achieve after surgery or biopsy, while it would be helpful for neurosurgeons to make individual operation plan if the malignant degrees of different parts of tumors can be identified before surgery. Meanwhile, in clinical practice, there are still difficulties in distinguishing gliomas from some other intracranial tumors, such as primary central nervous system lymphomas (PCNSL). The treatments for PCNSL and gliomas are totally different. Therefore, more precise differential diagnosis of gliomas before surgery can help to avoid unnecessary and costly surgery.

Diffusion-weighted imaging (DWI) is a noninvasive method to evaluate water diffusion in tissues. Several models have been developed to fit multi-b-value DWI, such as stretched-exponential model, bi-exponential model, and kurtosis model. Many studies based on the bi-exponential model have been showed a potential value in grading gliomas and distinguishing PCNSL from gliomas.4–6 However, the bi-exponential model has been challenged for its lack of reproducibility,7 and has been considered as oversimplified.8 Several previous studies have indicated the existence of water molecular pool with extremely low diffusion in tissues.9–12 Recently, we have proposed a theoretical modified tri-exponential model for multi-b-value DWI to measure the cytoplasmic organelle water fraction (COWF).13 COWF means the proportion of water molecules in...
the cytoplasmic organelles to the total water molecules in the tissue. Higher degree of malignancy is always associated with higher cell density in tumors. Besides, swollen cytoplasmic organelles have been detected in highly malignant tumors,[14,15] which may be due to vigorous metabolism and relative hypoxia. Hence, COWF may have a positive association with malignant degree of tumors. We performed this preliminary study to investigate the clinical value of the COWF map derived using the modified tri-exponential model in evaluating the malignant degree of gliomas and distinguishing PCNSL from gliomas.

2. Materials and methods

2.1. Patient selection
This retrospective study was based on our prospectively collected database for consecutive patients with gliomas who were hospitalized at our center between August 2013 and January 2015. This study was approved by the institutional review board of our center. Written informed consents were obtained from all participants. All clinical investigations were conducted according to the principles expressed in the Declaration of Helsinki. This study enrolled patients who

1. underwent a pre-operative MRI examination with a multi-b-value DWI;
2. had a diffusion glioma or PCNSL confirmed by pathologists who were blinded to clinical information.

WHO grade II gliomas are considered as low-grade gliomas (LGG), while WHO grade III and WHO grade IV gliomas are regarded as HGG. The Ki-67 index was examined in 47 glioma patients.

2.2. Image data acquisition
The patients were all imaged pre-operatively using a 3.0-T MR system (Discovery MR750, GE Healthcare Systems, Milwaukee, WI) with an 8-channel high-resolution receiver head coil. The DWI sequence was acquired with 9 b-values (0, 100, 200, 300, 500, 700, 1000, 2000, and 3000 s/mm²) in three orthogonal directions using a single-shot echo planar imaging with the following parameters: repetition time/echo time, 3000/88.6 ms; section thickness, 4 mm; spacing between slices, 5 mm; field of view, 240 × 240 mm; matrix, 256 × 256; phase FOV, 1.00; flip angle, 90; and pixel bandwidth, 1953.1 Hz/pixel. The number of scan averages varied from one for b = 0 s/mm² to six for b = 3000 s/mm². The scan time of the DWI sequence was 3 min 6 s. In addition, a contrast-enhanced T2-flair sequence was also performed with the same sections after the injection of gadodiamide (Omniscan, Nycomed Imaging, Oslo, Norway) with a dose of 10 mL.

2.3. Model
The modified tri-exponential mode contains three compartments: the strictly diffusion-limited compartment, slow diffusion compartment, and fast diffusion compartment. Theoretically, the strictly diffusion-limited compartment represents water molecules strictly limited in cytoplasmic organelles with extremely small space, and the slow diffusion compartment represents water molecules in cytoplasmic matrix and cell nucleus, while the fast diffusion compartment represents extracellular water molecules.[13] The equation of the modified tri-exponential model is expressed as follows:

\[
\frac{S_b}{S_0} = f_0 + f_{\text{slow}} e^{-\frac{b}{\text{ADC}_{\text{slow}}}} + f_{\text{fast}} e^{-\frac{b}{\text{ADC}_{\text{fast}}}} + f_0 + f_{\text{slow}} + f_{\text{fast}} = 1
\]

where S represents the signal intensity at corresponding b, and S₀ represents the signal intensity at b = 0 s/mm², and f₀, fslow, and ffast represent the fractions of the strictly diffusion-limited compartment, slow diffusion compartment and fast diffusion compartment, respectively. Here, we termed f₀ map as COWF map.

2.4. Image processing and analysis
Parametric maps were generated using the method described detailed in a previous study.[13] The regions of interest (ROI) were volumetric, manually placed slice by slice on the DWI images with b = 3000 s/mm² by an experienced neuroradiologist with 20 years’ experience who was blinded to patients’ clinical information. The solid tumor areas were included in the ROIs as many as possible, while the regions of necrosis, cystic lesions and hematoma were excluded carefully. Then, the ROIs were copied to the parameter maps, and the mean COWF, fslow, fast, ADCslow and ADCfast values were calculated for each ROI. In addition, ROIs were also drawn by a junior neurosurgeon, and the mean values of the parameters were calculated in order to assess the interobserver concordance.

2.5. Statistical analysis
All statistical analyses were performed with SPSS version 22 (IBM, Armonk, New York, NY). The intraclass correlation coefficient was used to assess interobserver concordance for the measurement of the parameters. KS normality test was used to test whether the parameters obey normal distribution. One-way ANOVA followed by LSD test was used to compare difference among three groups. Receiver operating characteristic (ROC) curves were generated for parameters in differentiating HGG from LGG and differentiating PCNSL from gliomas. The area under the curve (AUC), sensitivity, specificity, and best cut-off value were determined for each parameter. Pearson correlation analysis was performed to investigate the correlations between the parameters and the Ki-67 index. A value of P < .05 was regarded as statistically significant.

3. Results

3.1. Patient characteristics
A total of 66 patients (females, 28 [41.2%]; age, 50 ± 21 years) were enrolled, including 61 gliomas (females, 27 [44.2%]; age, 49 ± 21 years) and 5 PCNSL (female, 1 [20%]; age, 60 ± 12 years). Among these gliomas, there were 16 LGG and 45 HGG (WHO grade II, 16; WHO grade III, 17; WHO grade IV, 28).

3.2. Interobserver concordance
Manifestations of LGG, HGG, and PCNSL in parametric maps generated using the modified tri-exponential model are shown in Figure 1. The intraclass correlation coefficients for the measurements of the mean COWF, fslow, fast, ADCslow, and

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ADC$_{fast}$ values were 0.944, 0.843, 0.899, 0.875, and 0.863, respectively.

### 3.3. Parameters in each tumor group

Figure 2 shows the box plots of parameters of different grades of gliomas and PCNSL. The COWF value had an obviously increasing tendency with the grade of gliomas, while $f_{fast}$ and ADC$_{slow}$ had decreasing tendencies. There was no significant difference in ADC$_{fast}$ between any pairs of subgroups. The mean COWF values were significantly different among LGG (3.1% ± 1.4%), HGG (6.9% ± 2.8%), and PCNSL (14.0% ± 2.2%) ($P < .001$), shown in Table 1. The mean COWF value was significantly higher in PCNSL than in HGG ($P < .001$), and also significantly higher in HGG than in LGG ($P < .001$). On the contrary, the mean $f_{fast}$ value was significantly lower in PCNSL than in HGG ($P < .001$), and also significantly lower in HGG than in LGG ($P < .001$). When compared with LGG, PCNSL, and HGG had significantly higher mean $f_{slow}$ value ($P = .032$ and .042, respectively) and significantly lower mean ADC$_{slow}$ value (both $P < .001$). There was no significant difference in the mean ADC$_{fast}$ value among LGG, HGG, and PCNSL.

### 3.4. ROC analysis

The ROC curves of parameters in distinguishing HGG from LGG and in distinguishing PCNSL from gliomas are shown in Figure 3. The AUC, cutoff value, sensitivity and specificity of the mean COWF value were 0.899, 4.0%, 84.4%, and 81.3%, respectively, in distinguishing HGG from LGG; and were 0.646, 0.941, and 0.839, respectively, in distinguishing PCNSL from gliomas.

### 3.5. Correlation with the Ki-67 index

Figure 4 demonstrates the correlations between the mean parameter values and the Ki-67 index. The mean COWF value had a moderate correlation with the Ki-67 index ($r = 0.647$, $P < .001$). Meanwhile, the mean $f_{slow}$ value ($r = 0.421$, $P = .003$), $f_{fast}$ value ($r = 0.583$, $P < .001$), ADC$_{slow}$ value ($r = 0.476$, $P < .001$) showed mild correlations with the Ki-67 index. There were no significant association between the mean ADC$_{fast}$ value and the Ki-67 index ($P = .201$).

### 4. Discussion

In the present study, four parametric maps (COWF, $f_{slow}$, $f_{fast}$, ADC$_{slow}$) derived using the new model were found to be effective in grading gliomas and distinguishing PCNSL from gliomas. Besides, these parameters also showed significant correlations with the Ki-67 index. The COWF, a new parameter representing cytoplasmic organelle water fraction, showed the highest clinical value among all the parameters of the model. Particularly, when compared with the ADC$_{1000}$ and ADC$_{3000}$ maps as previously reported,$^{[16]}$ the COWF map was found to be more useful in evaluating the grade and proliferation activity of gliomas.

In the present study, we found that the COWF value dramatically increased with the grade of gliomas. In gliomas, the swelling mitochondria and dilated cisterns of endoplasmic reticulum have been detected by previous studies.$^{[14,15]}$ Besides,
significant differences in microstructure have been spotted out among different malignant degrees of gliomas.\textsuperscript{[17]} Other microstructure changes including swollen mitochondria, distended Golgi complex, and distended endoplasmic reticulum have been detected in glioblastomas.\textsuperscript{[18,19]} As for PCNSL, polysomes, and rough endoplasmic reticulum were found to be abound in lymphoblastomas.\textsuperscript{[20]} Accordingly, the fraction of water molecules strictly limited in cytoplasmic organelles may increase and become a significant compartment in high-malignant tumors.

According to previous studies, minimum ADC value derived by the mono-exponential model was smaller in HGG than in LGG.\textsuperscript{[21,22]} Previous studies have also shown that lower ADC value correlated well with higher cellularity.\textsuperscript{[23,24]} The hypothesis proposed in previous studies is that tumor tissue with high cellularity decreases in extracellular space resulting in a decreased ADC value.\textsuperscript{[21,22]} HGG has higher cellularity than LGG, while PCNSL has even higher cellularity than gliomas.\textsuperscript{[21,22,25]} In the present study, the $f_{\text{fast}}$ value, which represents the volume fraction of extracellular space, decreased with the grade of gliomas increasing, and was even lower in PCNSL than in gliomas. These findings in the present study are consistent with the facts that the extra-cellular space is smaller in PCNSL than in HGG and also smaller in HGG than in LGG, demonstrating that the new model may reveal more detailed microstructure characters of tumor tissues.

Table 1

| Parameters | LGG | HGG | PCNSL |
|-----------|-----|-----|-------|
| $C_{\text{OWF}}$ (%) | $3.1 \pm 1.4$ | $6.9 \pm 2.8$ | $14.0 \pm 2.2$ |
| $f_{\text{slow}}$ (%) | $47.6 \pm 2.8$ | $49.8 \pm 3.6$ | $51.4 \pm 5.6$ |
| $f_{\text{fast}}$ (%) | $49.3 \pm 3.4$ | $43.3 \pm 5.6$ | $34.7 \pm 4.6$ |
| $A_{\text{ADC}_{\text{slow}}}$ ($10^{-6} \text{mm}^2/\text{s}$) | $1178 \pm 287$ | $864 \pm 257$ | $609 \pm 301$ |
| $A_{\text{ADC}_{\text{fast}}}$ ($10^{-6} \text{mm}^2/\text{s}$) | $2045 \pm 311$ | $2036 \pm 388$ | $1901 \pm 206$ |

$C_{\text{OWF}}$ = cytoplasmic organelle water fraction, HGG = high grade gliomas, LGG = low-grade gliomas, PCNSL = primary central nervous system lymphomas.

\textsuperscript{a} $P < .05$.

\textsuperscript{b} $P < .001$, compared with LGG.

\textsuperscript{c} $P < .05$.

\textsuperscript{d} $P < .001$, compared with HGG.
studies have pointed out that high b-value DWI maps are more valuable in distinguishing the degree of malignancy of tumors.\textsuperscript{[16,21,29,30]} However, the potential mechanisms are not clarified. According to the modified tri-exponential model, signal intensity of the strictly diffusion-limited compartment will still remain unchanged at high b-values, while signal intensities of other two compartments will decrease dramatically. As a result, signal intensities on high b-value DWI maps may majorly originate from the strictly diffusion-limited compartment. This might be the reason why high b-value DWI maps are more effective in malignancy grading of tumors than normal b-value DWI maps. As high b-value DWI maps have also been found to be more helpful in several other aspects of tumor evaluation,\textsuperscript{[16,31,32]} further researches are needed to investigate the clinical value of the modified tri-exponential model in more aspects of tumor evaluation.

There are several limitations in this preliminary study. First, although the data were prospectively collected, this retrospective study might have a potential risk of selection bias. Second, the number of PCNSL was small, and this was not persuasive enough for determining the clinical value in distinguishing PCNSL from gliomas. Besides, the diagnostic accuracy of the COWF map in distinguishing HGG from LGG did not verified by a validation group. Further studies enrolling larger samples are needed to verify the diagnostic accuracy of the COWF map in distinguishing PCNSL from gliomas and distinguishing HGG from LGG. Third, this was a retrospective study and the scanning parameters were not optimized. The clinical value of the new model may be further improved after optimizing scanning parameters.

In conclusion, the strictly diffusion-limited compartment is a significant component in PCNSL and HGG. The modified tri-exponential model may provide more detailed information about water diffusion in tumors tissues. The COWF maps derived using the modified tri-exponential model has potential value in preoperative evaluating the grade and proliferation activity of gliomas and distinguishing PCNSL from gliomas. Further studies are needed to verify the clinical value of the COWF maps in tumor evaluations.

### Table 2

| Parameters | AUC  | Sensitivity (%) | Specificity (%) | Cutoff values |
|------------|------|-----------------|-----------------|---------------|
| HGG vs LGG |      |                 |                 |               |
| COWF       | 0.899| 84.4            | 81.3            | 4.0           |
| f\textsubscript{slow} | 0.704| 51.1            | 93.8            | 50.8          |
| f\textsubscript{fast} | 0.820| 62.2            | 100             | 45.2          |
| ADC\textsubscript{slow} | 0.798| 64.4            | 87.5            | 926           |
| PCNSL vs gliomas |      |                 |                 |               |
| COWF       | 0.980| 100             | 96.7            | 12.1          |
| f\textsubscript{slow} | 0.646| 80.0            | 63.9            | 50.9          |
| f\textsubscript{fast} | 0.941| 100             | 85.3            | 40.2          |
| ADC\textsubscript{slow} | 0.839| 80.0            | 96.7            | 524.5         |

The unit of COWF, f\textsubscript{slow} and f\textsubscript{fast} is %; the unit of ADC\textsubscript{slow} is ×10\textsuperscript{-6}mm\textsuperscript{2}/s.

AUC = area under the curve, COWF = cytoplasmic organelle water fraction, HGG = high grade gliomas, LGG = low-grade gliomas, PCNSL = primary central nervous system lymphomas.
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