The normal growth of the tracheal wall in human foetuses

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A b s t r a c t

Introduction: Tracheal wall thickness is a substantial indicator in various pathological changes. The present study was performed to compile normative data and formulae for the tracheal wall thickness and volume at varying gestational age.

Material and methods: Using anatomical dissection, digital image analysis and statistics a range of the wall thickness, proximal internal-to-external cross-sectional area ratio, and wall volume for the trachea in 73 spontaneously aborted human fetuses aged 14-25 weeks was examined.

Results: No significant male-female differences were found. The values of tracheal wall thickness ranged from 0.36 ±0.01 mm for the 14-week group to 1.23 ±0.17 mm for the 25-week group of gestation, according to the linear function \( y = -0.823 + 0.083 \times \text{age} \pm 0.087 \). The tracheal lumen rate, expressed as the proximal internal-to-external cross-sectional area ratio, decreased from 42.61 ±1.11% to 26.78 ±4.95%, according to the function \( y = 62.239 - 1.487 \times \text{age} \pm 3.119 \). The tracheal wall volume rose from 16.28 ±4.18 mm\(^3\) in fetuses aged 14 weeks to 269.22 ±29.26 mm\(^3\) in fetuses aged 25 weeks, according to the quintic function \( y = 0.000052 \times \text{age}^{4.894} \).

Conclusions: The tracheal wall parameters show no sexual dimorphism. The tracheal wall grows linearly in its length, and according to a quintic function in its volume. A relative decrease in the tracheal lumen at the expense of an increase in both the wall thickness and wall volume of the trachea is found during gestation.

Key words: trachea, wall thickness, wall volume, tracheal lumen rate, regression analysis.

Introduction

Advances in perinatal medicine have required an exhaustive knowledge of the normal growth of fetal airway development to determine normal and pathological criteria adapted to anatomical particularities of the fetal tracheo-bronchial tree [1-6]. Tracheal wall thickness is a substantial indicator in various pathological changes [7-9]. Both increased airway wall thickness and smaller airway lumen have been relatively well examined in patients with asthma or chronic obstructive pulmonary disease [10-12]. A thickened tracheo-bronchial wall, the morphological substratum of most airway diseases, can be assessed in vivo by multi-detector computed tomography [13].
To date, a few theoretical patterns of fetal tracheal morphometry have focused on its length [5, 14-16], external [15, 17] or internal [5, 14, 18-22] transverse diameters, and external [17] or internal [18, 23] volumes. However, neither wall thickness nor wall volume of the trachea have been reported in human fetuses.

In order to supplement the missing information on the tracheal wall in human fetuses, our objectives were to examine: age-specific reference intervals for wall thickness, and wall volume at varying gestational ages, relative growth of the tracheal lumen, the growth curves for wall thickness and wall volume.

Material and methods

Material

The study was performed on 73 human fetuses of both sexes (39 male, 34 female) of Caucasian origin, which had been derived from spontaneous abortions or stillbirths in the years 1989-2001. The sample included fetuses which were the outcome of causes of intra-uterine growth restriction. Legal and ethical considerations were consistent with the rules of the University Research Ethics Committee (KB 189/2011). On macroscopic examination the fetuses were free of malformation affecting laryngo-tracheal structures and never intubated. The gestational age varied from 14 to 25 weeks (Table I). The fetal ages were accurately established on the basis of the following criteria: 1) gestational age based on measurements of the crown-rump length [24], 2) known date of the beginning of the last menstrual period, and 3) a combination of abdominal circumference, femur length and biparietal diameter determined by early second-trimester ultrasound scan. All specimens had been immersed in 10% neutral buffered formalin solution for 12-24 months for preservation, and then dissected under 10-fold magnification using a stereoscope with Huygens ocular.

Measurements

In each fetus, the trachea in situ with a millimetre scale was placed vertically to the optical lens axis, then recorded using a Nikon D200 camera, and digitalized to TIFF images (Figure 1). Next, digital pictures of the trachea were assessed using digital image analysis (NIS-Elements BR 3.0, Nikon), which semi-automatically estimated the four examined variables: tracheal length, wall thickness, proximal external cross-sectional area and proximal internal cross-sectional area. Digital image analysis turned out to be an excellent method of determining the parameters mentioned above, because tracheal length, tracheal wall thickness, and internal and external cross-sectional areas of the trachea could be accurately traced using a cursor.

At first, tracheal length was measured, being expressed as the distance between the superior border of the first tracheal cartilage and the tracheal bifurcation. After that the cross section was taken between the cricoid cartilage and the first tracheal ring to examine the geometry of the proximal cross-sectional area of the trachea, i.e. wall thickness, proximal external cross-sectional area, and proximal internal cross-sectional area (Figure 2). Tracheal wall thickness constituted the distance between its internal and external borders at the level of the first tracheal ring. Both internal and external cross-sectional areas of the trachea were

![Table I. Distribution of fetuses studied](image_url)

| Fetal age | Crown-rump length [mm] | Number | Sex |
|-----------|------------------------|--------|-----|
| Months    | Weeks [Hdb-life]       | Mean   | SD  | Min | Max | Male | Female |
| 4         | 14                     | 79.5   | 4.3 | 76.0 | 81.0 | 2    | 1     | 1     |
|           | 15                     | 89.3   | 6.4 | 84.0 | 93.0 | 1    | 1     | 0     |
|           | 16                     | 103.1  | 6.3 | 96.0 | 108.0| 2    | 1     | 1     |
| 5         | 17                     | 114.0  | 7.3 | 110.0| 123.0| 9    | 5     | 4     |
|           | 18                     | 129.5  | 6.8 | 124.0| 136.0| 10   | 5     | 5     |
|           | 19                     | 141.9  | 5.9 | 138.0| 149.0| 7    | 4     | 3     |
|           | 20                     | 155.0  | 5.2 | 152.0| 162.0| 13   | 7     | 6     |
| 6         | 21                     | 166.4  | 4.9 | 165.0| 174.0| 11   | 6     | 5     |
|           | 22                     | 178.9  | 7.2 | 175.0| 185.0| 5    | 2     | 3     |
|           | 23                     | 192.9  | 7.2 | 187.0| 195.0| 6    | 3     | 3     |
|           | 24                     | 201.4  | 4.2 | 199.0| 204.0| 5    | 3     | 2     |
| 7         | 25                     | 214.8  | 4.7 | 212.0| 217.0| 2    | 1     | 1     |
| Total     |                        | 73     | 39  | 34   |      |
semi-automatically measured, after tracing around internal and external borders of the first tracheal cartilage, respectively.

Because the size of specimens varied, we calculated the proximal internal-to-external cross-sectional area ratio, so as to express the relative growth...
of the tracheal lumen. In order to calculate the tracheal wall volume, tracheal wall thickness was assumed to be uniform in size along its length. Thus, the tracheal wall volume could be described by the following formula:

\[ V = V_e - V_i = eCSA \times l - iCSA \times l = (eCSA - iCSA) \times l, \]

\[ Ve, Vi \] – tracheal wall volume, \[ Ve, Vi \] – external volume of the trachea, \[ eCSA \] – proximal external cross-sectional area, \[ iCSA \] – proximal internal cross-sectional area, \[ l \] – tracheal length.

For each fetus, the six following measurements and calculations of the trachea were done:

- length in mm, corresponding to the distance from the superior border of the first tracheal cartilage to the inferior border of the tracheal bifurcation,
- wall thickness in mm, measured at the level of the first tracheal cartilage,
- proximal external cross-sectional area in mm², traced around the external border of the first tracheal cartilage,
- proximal internal cross-sectional area in mm², traced around the internal border of the first tracheal cartilage,
- proximal internal-to-external cross-sectional area ratio (tracheal lumen rate),
- tracheal wall volume in mm³, calculated as the product of the difference between proximal external and internal cross-sectional areas multiplied by the length.

In order to minimize measurement and observer bias, all the measurements were performed by one researcher. The mean of three repeated measurements was taken for each variable to minimize intra-observer variation.

**Statistical analysis**

The differences between the repeated measurements, as the intra-observer variation, were evaluated by the Wilcoxon signed-rank test. Both the tracheal wall thickness and the tracheal wall volume were plotted against fetal age so as to establish their growth. As the first step in the statistical analysis, Student’s t-test was used to examine the influence of sex on the values of the parameters studied. Of note, the growing fetuses were separated into 12 intervals not equally distributed with respect to gestational age. Because 2 tracheas were included in the gestational ages of 14, 16 and 25 weeks, and only 1 trachea in the gestational age of 15 weeks, which clearly did not represent adequate samples, the first three intervals (14-16 weeks), and the last two intervals (24-25 weeks) were separately grouped. So, in order to examine sexual differences we tested possible differences between the nine following age groups: 14-16, 17, 18, 19, 20, 21, 22, 23

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**Table II. Morphometric parameters of the trachea**

| Fetal age [weeks] | Number of fetuses | Wall thickness [mm] | Proximal internal-to-external cross sectional area ratio [%] | Wall volume [mm³] |
|-------------------|-------------------|---------------------|----------------------------------------------------------|------------------|
|                   |                   | Mean                | SD            | Mean                   | SD            | Mean                   | SD            |
| 14                | 2                 | 0.36                | 0.01          | 42.61                 | 1.11          | 16.28                  | 4.18          |
| 15                | 1                 | 0.43                | 0.00          | 41.30                 | 0.00          | 26.85                  | 0.0           |
| 16                | 2                 | 0.48                | 0.08          | 40.10                 | 6.90          | 247.22                 | 15.63         |
| 17                | 9                 | 0.55                | 0.06          | 36.57                 | 2.27          | 52.73                  | 10.87         |
|                   |                   | (p < 0.01)          |               | (p < 0.01)            |               | (p < 0.05)             |               |
| 18                | 10                | 0.65                | 0.08          | 36.07                 | 3.96          | 79.72                  | 15.63         |
|                   |                   | (p < 0.01)          |               | (p < 0.01)            |               | (p < 0.01)             |               |
| 19                | 7                 | 0.78                | 0.08          | 32.62                 | 2.48          | 119.14                 | 28.50         |
|                   |                   | (p > 0.05)          |               | (p < 0.05)            |               | (p < 0.01)             |               |
| 20                | 13                | 0.80                | 0.07          | 31.46                 | 2.45          | 126.32                 | 26.74         |
|                   |                   | (p < 0.01)          |               | (p < 0.01)            |               | (p < 0.01)             |               |
| 21                | 11                | 0.86                | 0.11          | 30.67                 | 2.69          | 152.24                 | 37.46         |
|                   |                   | (p < 0.01)          |               | (p < 0.01)            |               | (p < 0.01)             |               |
| 22                | 5                 | 0.97                | 0.07          | 29.08                 | 3.91          | 202.85                 | 23.48         |
|                   |                   | (p < 0.05)          |               | (p < 0.05)            |               | (p < 0.01)             |               |
| 23                | 6                 | 1.02                | 0.16          | 28.77                 | 2.54          | 220.34                 | 60.94         |
|                   |                   | (p < 0.01)          |               | (p < 0.01)            |               | (p < 0.05)             |               |
| 24                | 5                 | 1.17                | 0.11          | 27.13                 | 6.48          | 247.22                 | 99.38         |
| 25                | 2                 | 1.23                | 0.17          | 26.78                 | 4.95          | 269.22                 | 29.26         |

The means in columns differ significantly (\( p < 0.05 \) or \( p < 0.01 \)), as indicated above.
and 24–25 weeks. Furthermore, we tested possible sex differences for the whole group, without taking into account the fetal age. In order to test whether the different variables significantly changed with age the one-way ANOVA test and post-hoc Bonferroni test were used for the nine groups (Table II). Linear and nonlinear regression analysis was used to derive the curve of best fit for each parameter against gestational age. Coefficients of determination ($R^2$) between each parameter and fetal age were estimated. Differences were considered significant at $p < 0.05$.

**Results**

No statistically significant differences were found in the evaluation of intra-observer reproducibility of the tracheal wall measurements ($p > 0.05$). In turn, inter-observer variability was not assessed since all the measurements were done by one observer. The statistical analysis showed no sexual differences ($p > 0.05$), so the numerical results without regard to sex have been presented in Table II. In contrast, the growth curves of best fit for each parameter plotted against gestational age were statistically significant ($p < 0.05$).

The values of tracheal wall thickness ranged from 0.36 ±0.01 mm for the 14-week group to 1.23 ±0.17 mm for the 25-week group of gestation. The tracheal wall thickness in relation to gestational age in weeks (Figure 3) was consistent with the first-degree polynomial (linear) function $y = -0.823 + 0.083 \times$ age ±0.087 ($R^2 = 0.83$).

During the study period, the tracheal lumen rate (Figure 4), expressed as the proximal internal-to-external cross-sectional area ratio, decreased from 42.61 ±11.11% to 26.78 ±4.95%, according to the first-degree polynomial (linear) function $y = 62.239 - 1.487 \times$ age ±3.119 ($R^2 = 0.56$). An increase in the tracheal wall thickness was accompanied by a decrease in the tracheal lumen (Figure 5).

At the same time, the tracheal wall volume rose from 16.28 ±4.18 mm$^3$ in fetuses aged 14 weeks to 269.22 ±29.26 mm$^3$ in fetuses aged 25 weeks. The numerical data of tracheal wall volume followed in accordance with the logarithmic function ln ($y$) = -9.873 + 4.894 × ln (age) ±0.212 ($R^2 = 0.91$). After a mathematical transformation this logarithmic function was equivalent to the fifth-degree polynomial (quintic) function $y = 0.000052 \times$ age$^{4.894}$ (Figure 6). Figure 7 summarizes the volumetric pro-
portions between the wall and lumen of the growing trachea in human fetuses.

Discussion

The present paper caps the morphometric study of the fetal trachea, some results of which concerning both external (length, proximal external cross-sectional area, external volume) and internal (proximal cross-sectional area, internal volume) parameters have recently been published [17, 18]. Because of this, three tracheal parameters — length, proximal external cross-sectional area, and proximal internal cross-sectional area — were excluded from Table II. Inasmuch as wall thickness was independently measured in a direct way using digital image analysis, both the tracheal lumen rate and tracheal wall volume were not directly assessed, but calculated taking into account the results previously reported [17, 18]. Obviously, the tracheal wall volume may have been considered as the difference between the external and internal volumes of the trachea, resulting in the formula $V = (eCSA - iCSA) \times l$.

Of note, the present data are the first to highlight the quantitative analysis of the growing tracheal wall in human fetuses. The fetal material was relatively numerous ($n = 73$), comparable, and representative of the studied population. Furthermore, a valid objective software package (NIS Elements BR 3.0, Nikon) was used for measuring wall thickness, the lumen rate and wall volume of the trachea. Our results have been real, because tissue shrinkage related to formalin fixation had little (0.5-10%) influence on the tracheal measurements taken in situ [25, 26]. On the other hand, isolated segments of the trachea which had been immersed in 10% formalin solution were prone to artefacts and 10% shrinkage [21].

There were no differences between males and females for tracheal wall measurements, in keeping with the results concerning other morphometric parameters such as length [5, 14, 15], external [15, 17] or internal [5, 14, 18-21] transverse diameters, and external [17] or internal [18, 20] volumes of the fetal trachea. Some authors [5, 20] reported that male and female infants and prepubertal boys and girls had similar tracheal dimensions, in spite of the fact that boys were taller. Tracheal diameters continued to grow after tracheal length had plateaued in teenage boys, and significant sexual differences in tracheal dimensions emerged as late as at puberty [20].

Anatomical measurements of tracheal wall thickness were characterized by a quasi-linear evolution from $0.36 \pm 0.01$ mm to $1.23 \pm 0.17$ mm for fetuses at the age of 14 and 25 weeks, respectively. The linear model chosen for age-specific reference intervals for wall thickness was $y = -0.823 + 0.083x$ age $\pm 0.087$, because the highest determination coefficients for possible square root ($R^2 = 0.26$) and quadratic ($R^2 = 0.24$) functions were much smaller than that ($R^2 = 0.83$) of the linear one. It is noteworthy that in fetuses at ages of 14 and 25 weeks of gestation a 3-fold increase in tracheal wall thickness was accompanied by a simultaneous decrease in the tracheal lumen rate from $42.61 \pm 1.11\%$ to $26.78 \pm 4.95\%$. Thus, during normal development the tracheal wall thickness increased at the expense of the decreasing tracheal lumen (Figure 5). The same trend to smaller airway lumen and increased wall thickness of the trachea has been proven in different pathological changes.

We would like to correlate the influence of tracheal thickness with particular examples of pathological changes, so as to stress the importance of our tracheal measurements. Both increased airway wall thickness and smaller airway lumen have been relatively well examined in patients with asthma, chronic obstructive pulmonary disease and cumulative smoking history [11, 12]. The thickening and
remodelling of large airways was reported to closely correspond with the severity of asthma [10, 11]. The degree of airflow obstruction is caused by an enlargement of the mucous glands with increased secretion responsible for mucous plugging, atrophy or inflammation of tracheal cartilages [27].

Diesel exposure may have a key role in an increase in tracheal thickness at the expense of its luminal diameter [27, 28]. According to Nakano et al. [27] and Safak et al. [28], the tracheal walls of toll collectors were dependent on the working duration, being significantly thicker in those working for 11-15 years than 0-10 years. Of note, tracheo-bronchial wall thickening was reported in elderly smokers with no respiratory symptoms [29]. Some authors [30, 31] have proved in animal models that exposure to the most important air pollutant, i.e. SO₂, brought about increased tracheal wall thickness due to hypertrophy of tracheal submucosal glands, epithelial mucous cell hyperplasia or metaplasia.

Tracheal involvement in many diseases is characterized by increased tracheal wall thickness due to:

• diffuse calcified nodular thickening of the tracheal wall and nodularity of its mucosa in rhinoscleroma [32],
• multiple submucosal osteocartilaginous nodules and thickening of tracheal cartilaginous rings in tracheobronchopathia osteochondroplastica [32],
• deposition of amyloid fibrils in the submucosa in tracheobronchial amyloidosis [32],
• recurrent inflammation of tracheal rings in relapsing polychondritis [32],
• granulomatous infection in tuberculosis [32],
• osseocalcineus metaplasia of the tracheal rings [32-35],
• adenoid cystic carcinomas [36].

The volumetric growth of the tracheal wall, from 16.28 ±4.18 mm³ in fetuses aged 14 weeks to 269.22 ±29.26 mm³ in fetuses aged 25 weeks, was fitted satisfactorily in accordance with the fifth-degree polynomial (quintic) function

\[ y = 0.000052 \times \text{age}^{5.764}. \]

According to this model, the tracheal wall volume, as the most dynamic parameter, was strongly increasing with fetal age, by 10.57 mm³ during the 14-week period, and by 22 mm³ during the 24-week period. The lack of data on the studied parameters in the professional literature obviously limited discussion on this subject.

The main limitation of this study was the relatively narrow age range of fetuses. The equations that we propose need to be checked in fetuses with a wide age range. Another limitation of the present study was that all measurements were conducted by a single observer in a blind fashion.

This study provides completely novel, accurate data on tracheal wall thickness and tracheal wall volume at varying gestational ages. We believe that the present data, when appropriately interpreted, might be potentially useful in the diagnosis and monitoring of fetal and perinatal tracheobronchial disorders.

In conclusions, the tracheal wall parameters show no sexual dimorphism. The tracheal wall grows linearly in its length, and according to a fifth-degree polynomial function in its volume. A relative decrease in the tracheal lumen at the expense of an increase in both the wall thickness and wall volume of the trachea is found during gestation.

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