behavioral/cognitive

Cascaded Tuning to Amplitude Modulation for Natural Sound Recognition

Takuya Koumura, Hiroki Terashima, and Shigeto Furukawa
NTT Communication Science Laboratories, Atsugi, Kanagawa, Japan 243-0198

The auditory system converts the physical properties of a sound waveform to neural activities and processes them for recognition. During the process, the tuning to amplitude modulation (AM) is successively transformed by a cascade of brain regions. To test the functional significance of the AM tuning, we conducted single-unit recording in a deep neural network (DNN) trained for natural sound recognition. We calculated the AM representation in the DNN and quantitatively compared it with those reported in previous neurophysiological studies. We found that an auditory-system-like AM tuning emerges in the optimized DNN. Better-recognizing models showed greater similarity to the auditory system. We isolated the factors forming the AM representation in the different brain regions. Because the model was not designed to reproduce any anatomical or physiological properties of the auditory system other than the cascading architecture, the observed similarity suggests that the AM tuning in the auditory system might also be an emergent property for natural sound recognition during evolution and development.

Key words: amplitude modulation; deep neural network; neural tuning; single-unit recording

Introduction

Natural sounds such as speech and environmental sounds exhibit rich patterns of amplitude modulation (AM) (Fig. 1a) (Varnet et al., 2017). For example, humans can recognize speech content and identify daily sounds based on their AM patterns even if the fine temporal structure is substantially degraded (Dudley, 1939; Shannon et al., 1995; Gygi et al., 2004). The AM rate (i.e., the number of AM cycles per second) is one of the most important physical dimensions in auditory perception (Fig. 1b) (Houtgast and Steeneken, 1985). Psychophysical studies suggest that the sensitivity of the auditory system to AM can be accounted for by filtering mechanisms in the AM rate domain (Viemeister, 1979; Bacon and Grantham, 1989; Houtgast, 1989; Dau et al., 1997).

The auditory system converts the physical properties of a sound stimulus to neural activities and processes them through a cascade of brain regions (see Fig. 30–12 in Kandel et al., 2000). Neurophysiological studies have found a number of neurons and neural populations that tune to the AM rate (Joris et al., 2004; Liegeois-Chauvel et al., 2004; Sharpee et al., 2011). Some neurons fire synchronously with the stimulus AM waveform and the degree of synchrony depends on the AM rate (temporal coding of AM rate), whereas others encode the AM rate with their firing rates (rate coding of AM rate). Interestingly, the characteristics of AM tuning transform systematically along the processing stages from the periphery to the cortex (Joris et al., 2004; Sharpee et al., 2011): the AM rate with which neurons synchronize gradually decreases and the number of neurons that perform rate coding gradually increases (a phenomenon known as time-to-rate conversion).

Significance Statement

This study suggests that neural tuning to amplitude modulation may be a consequence of the auditory system evolving for natural sound recognition. We modeled the function of the entire auditory system; that is, recognizing sounds from raw waveforms with as few anatomical or physiological assumptions as possible. We analyzed the model using single-unit recording, which enabled a fair comparison with neurophysiological data with as few methodological biases as possible. Interestingly, our results imply that frequency decomposition in the inner ear might not be necessary for processing amplitude modulation. This implication could not have been obtained if we had used a model that assumes frequency decomposition.
Neurophysiological and theoretical studies have revealed how the auditory system works by exploring the neural mechanisms of the transformation of AM tuning (Hewitt and Meddis, 1994; Depireux et al., 2001; Zhang and Kelly, 2003; Guérin et al., 2006; Dicke et al., 2007; Mahajan et al., 2014). However, the functional significance of the transformation remains unknown. In other words, we still face the question of why the system has to be organized in that way.

Functional model of sensory systems

A computational approach with machine learning techniques is effective for explaining functional significance in sensory systems (Olshausen and Field, 1996; Lewicki, 2002; Terashima and Okada, 2012; Mlynarski and McDermott, 2017). The architectures and parameters of the models are trained to process natural stimuli for behaviorally relevant objectives with few assumptions regarding anatomical or physiological properties. Therefore, the trained model is expected to provide an effective representation of natural stimuli and if the representation is similar to that observed in a real sensory system, it is highly likely that the sensory system is also adapted to effectively processing sensory information for survival. In particular, a deep neural network (DNN) is one of the most successful models for both automatic data processing (Hinton et al., 2012; Krizhevsky et al., 2012; Schmidhuber, 2015) and explaining a neural representation of sensory information (Khaligh-Razavi and Kriegeskorte, 2014; Yamins et al., 2014; Horikawa and Kamitani, 2017; Zhuang et al., 2017; Cueva and Wei, 2018; Kell et al., 2018). A DNN consists of a cascade of layers with multiple units and a unit in a layer integrates the activations in a lower layer, which makes the model suitable for explaining the functions of cascaded brain regions.

In the present study, we optimized a DNN for natural sound recognition. To make a direct comparison of AM sensitivity in the DNN and that in the auditory system reported in a number of neurophysiological studies, we characterized the AM sensitivity of the DNN using standard neurophysiological methods by treating the DNN as if it were a biological brain. We showed the qualitative and quantitative similarities of the DNN to the auditory system.

Materials and Methods

Task. The task of the DNN was sound recognition. Specifically, the task was to estimate the sound category at the last time frame of a sound of a certain duration (0.19 s for natural sounds and 0.26 s for speech). Classification accuracy is defined as the average correct classification rate for each category, namely the number of time frames correctly estimated as a particular category divided by the total number of time frames in the category.

Datasets. Two datasets were used to train the DNNs. The first consisted of nonhuman natural sounds and is a subset of ESC-50 (Piczak, 2015). The original dataset contains 50 sound categories with 40 sounds for each category. From the original dataset, we used 18 categories of sounds not produced by human activity. Each entry in the original dataset contains a sound waveform with a length of <5 s and the sound category. In this study, we excluded silent intervals, resulting in a total length of 53.9 min. The original dataset is divided into five folds for cross-validation. We used fold #5 for validation and the other folds for training. The sound format was converted to 44.1 kHz 16-bit linear PCM.

The second dataset consisted of speech sounds (Garofolo et al., 1993). Each entry in the dataset contains the sound waveform of a single spoken sentence, categories of vocal elements, and the time intervals of each element. There were originally 61 categories. We merged some categories in accordance with previous studies (Lee and Hon, 1989; Lopes and Perdigao, 2011), resulting in 39 categories. The average and total durations of the sound were 3.1 s and 3.3 h, respectively. The data were originally divided into a validation set and a training set. In this study, we followed the original division. The validation and training sets contain the speech of 24 and 462 speakers, respectively. The speakers and sentences in the two divisions do not overlap. The sound format was 16 kHz 16-bit linear PCM.

Network architecture. Our DNN consisted of a stack of dilated convolutional layers (van den Oord et al., 2016) (Fig. 2), in which convolutional filters were evenly dilated in time. Convolution was conducted along the time axis. Each layer performed a dilated convolution on the activations of the previous layer and applied an activation function. The activation function was an exponential linear unit (Clevert et al., 2016). The first layer took samples of raw waveforms directly as an input. Each layer contained multiple units. All of the layers contained the same number of units for simplicity. The units in the highest layer were connected to the classification layer without convolution. The number of units in the classification layer was the same as the number of categories. The classification layer was omitted from the physiological analysis.

We used DNNs with 13 layers, each containing 128 units, for nonhuman sound and DNNs with 12 layers, each containing 64 units, for speech. The number of layers and the number of units in each layer were determined based on a pilot study and fixed throughout the study. In the pilot study, DNNs with various numbers of layers and units were trained using a random portion of the training set. The filter length was 2 and the dilation length was 2 to the power of the layer number (van den Oord et al., 2016). The number of layers and the number of units in each layer that gave the best classification accuracy on the other portion of the training set were used in the following study. We tested multiple architectures with random filter sizes and dilation lengths in each convolutional layer and selected the DNN that achieved the best classification accuracy on the novel dataset (Table 1). The filter size and dilation length were randomly chosen for each layer with certain constraints, namely that the filter size did not exceed 8 and the total input length for the whole DNN, which is equal to the length of the input time window of the topmost layer, did not exceed 8192 (~0.19 s) for nonhuman sound and 4096 (~0.26 s) for speech. The number of layers and the number of units in each layer were fixed as mentioned in the previous paragraph.

Optimization. The DNNs were trained on the training set and the classification accuracy was calculated for the validation set. The initial...
filter weights were randomly sampled and the biases were set to 0 in accordance with a previous study (He et al., 2015). The filter weights and biases were updated using the Eve algorithm (Koushik and Hayashi, 2016) with softmax cross entropy as the cost function. The number of iterations for a parameter update was determined as the value that gave the best classification accuracy on a random portion of the training set.

**Experimental design: physiological analysis of a DNN.** For a physiological analysis of a DNN, a sound stimulus was fed to the DNN and the values of each unit were recorded. The root mean square (RMS) of the input sound was adjusted approximately to the RMS of the training set. Before the analysis, 1 was added to the values of all the units because the minimum possible value of the activation function is \(-1\) (Clevert et al., 2016).

The stimulus was 8 s of sinusoidally amplitude-modulated white noise. In physiological studies, tuning to an AM rate is measured using sinusoidally amplitude-modulated tones with carriers at the neurons’ best acoustic frequency (AF, frequency of a sound waveform itself but not its amplitude envelope), sinusoidally amplitude-modulated white noises, or click trains. We did not use tones as carriers because many units showed multiple troughs in the AF tuning curves or nonmonotonic responses to the input amplitude, making it difficult to define the best AFs.

The synchrony to the stimulus and the average activity was calculated from the activations of each unit. The synchrony to the stimulus was quantified in terms of vector strength (Goldberg and Brown, 1969). When dealing with spike timing data recorded in neurons, each spike is represented as a unit vector with its angle corresponding to the modulator phase at that time and the vector strength is defined as the average length of these unit vectors. Equivalent operations were applied to the continuous output of the DNN unit to derive the vector strength (Eq. 1). The vector strength had a value between 0, indicating no synchrony, and 1, indicating perfect synchrony, as follows:

\[
\text{Vector strength} = \frac{\sum a(t) \cos(2 \pi f_{mt} t f)}{\left( \sum a(t) \cos(2 \pi f_{mt} t f) \right)^{\frac{1}{2}}},
\]

where \(t\) is an index of the time frame, \(a(t)\) is the unit activation, \(f_{mt}\) is the sampling rate, and \(f_{mt}\) is the stimulus AM rate. The average activity was defined as the temporal average of the values, which could be considered as the DNN version of an average spike rate. The synchrony and the average activity were averaged for 16 instances of the carrier white noise to reduce the effect of stimulus variability. A temporal modulation transfer function (tMTF) and a rate MTF (rMTF) were defined as the synchrony and average activity as functions of the AM rate, respectively. In physiology, an MTF is usually defined only at the AM rates at which the unit shows a statistically significant synchrony or spike rate. Because a statistical test on the results of a deterministic model such as our DNN makes no sense, we considered the synchrony or average activities below a certain threshold as “nonsignificant” and excluded them from the following analysis. The threshold was arbitrarily set at 0.01 for the synchrony and at 0.01 above the average activity in response to unmodulated white noise for the average activity.

An MTF was classified as one of the following four types: low-pass, high-pass, band-pass, or flat. A low-pass type MTF was defined as one that had no values smaller than 80% of its maximum for AM rates smaller than the peak rate. A high-pass type MTF was defined as one that had no values smaller than 80% of its maximum for rates larger than the peak rate. A flat MTF was defined as one that had no values smaller than 80% of its maximum or one with a peak to peak range of <0.1. The band-pass MTF was defined as being other than the above.

The best modulation frequencies (BMFs) were calculated from the band-pass type MTFs and the upper cutoff frequencies (UCFs) were calculated from the low-pass and band-pass type MTFs. The BMFs of low-pass, high-pass, or flat MTFs and the UCFs of high-pass or flat MTFs were considered to be impossible to define. The BMF was defined as the modulation rate at the peak of the MTF. If there were multiple peaks with the same height, the geometric mean of the rates was taken. The UCF was calculated in two different ways: one for qualitative visualization as shown in Figure 7a and the other for quantitative comparisons with specific physiological data for neurons found in the literature. The UCF for visualization was defined as the rate at which the MTF crosses 80% of its maximum value. If an MTF had multiple such rates, the geometric mean of the rates was used. The threshold of the UCF used for a quantitative comparison with the auditory system varied according to the reference physiology study. The thresholds were 50% (Eggermont, 1998; Zhang and Kelly, 2006), 80% (Rhode and Greenberg, 1994; Kuwada and Batra, 1999), and 70% (\(\sim 3\) DB) (Joris and Yin, 1992, 1998; Joris and Smith, 1998) of the maximum, 90%:10% interior division of its minimum and maximum (Krishna and Semple, 2000), an absolute value of 0.1 (Rhode and Greenberg, 1994; Zhao and Liang, 1995), and the highest rate that gives significant responses (Batra et al., 1989; Kuwada and Batra, 1999; Krishna and Semple, 2000; Lu and Wang, 2000; Lu et al., 2001; Liang et al., 2002; Batra, 2006; Bartlett and Wang, 2007; Scott et al., 2011). If there was no rate at which the MTF crossed the threshold, then the UCF was considered to be impossible to define.
The stimuli we used for calculating AF tuning were tones with various AFs and amplitudes. The activation of each unit was temporally averaged to obtain the response to a particular stimulus. The tuning curve was defined for each AF as the smallest amplitude inducing a response larger than a certain threshold. In physiological studies, thresholds are usually determined arbitrarily. Figure 15 shows tuning curves with thresholds of 0.001, 0.01, and 0.1.

Comparison with auditory system. We extracted the BMF and UCF distributions reported in previous physiological studies by digitizing the figures. If multiple figures were available, then we chose the clearest figure or that with the most neurons. The extracted values were used for a qualitative visualization in Figure 7c and a quantitative comparison with the DNNs. For the visualization, we averaged the distributions of all the subregions and all the neuron types in each region in each study. Then, the distributions in all the papers were averaged for each region. The resulting distributions were smoothed with a Gaussian filter with a width of 0.136 on a logarithmic scale of base 10. For quantitative comparison with a DNN, we calculated the similarity of each extracted distribution to the distribution of each layer in the DNN. As the measure of similarity, we used the Kolmogorov–Smirnov statistic subtracted from 1 because it is nonparametric and does not depend greatly on the bin widths of the histogram. For each BMF and UCF for each rate and temporal coding, we averaged the similarities in the same regions in a single study and then averaged the similarities in the same region in different studies. Averaging the four pairwise similarities (tBMF, tUCF, rBMF, and rUCF), we derived the final layer–region pairwise similarity matrix. Because no distribution of tBMF has been reported in auditory nerves (ANs); no distribution of rBMF has been reported in ANs, cochlear nucleus (CN), or superior olivary complex (SOC), and no distribution of rUCF has been reported in AN or CN, their similarities were set at 1 if there was no unit with a definable BMF or UCF and set at 0 otherwise. For regions other than these, the similarity was set at 0 if there was no unit with a definable BMF or UCF.

Evaluation of a pairwise similarity matrix. The similarity of the entire cascade and that of each layer were calculated from a pairwise similarity matrix. We wanted to evaluate the pairwise similarity matrix in a way in which high scores are obtained by a DNN with its lower, middle, and central brain regions, respectively. To realize this evaluation concept, we defined the cascade similarity as the weighted mean of the pairwise similarity matrix. We wanted to evaluate the pairwise similarity matrix in a way in which high scores are obtained by a DNN with its lower, middle, and central brain regions, respectively. To realize this evaluation concept, we defined the cascade similarity as the weighted mean of the pairwise similarity matrix. The weight at the cell \((i,j)\) was proportional to the following:

\[
1 - 2 \left( \frac{i-1}{N_i} \right) \left( \frac{j-1}{N_j} \right),
\]

where \(N_i\) and \(N_j\) are the number of brain regions (7) and the number of DNN layers, respectively. The weight was scaled so that the squared mean of the weight matrix was 1. The weight was maximal on the diagonal line and minimal in the top left and bottom right corners. The layerwise similarity was defined as the mean obtained in each layer.

Control experiments. In the first control experiment, the category labels of the sounds in the training set were randomly shuffled. The validation set was not modified. A parameter update was conducted for the same number of iterations as the original nonrandom condition. In the second control experiment, the waveform in each sound in the training set was randomly permuted, resulting in a noise-like input waveform maintaining only the marginal distribution of the amplitudes. The third control experiment was a waveform following task that involved copying the amplitude value of the last time frame of the input sound segment. To make the result directly comparable to those of the classification tasks, the target amplitude was quantized and we used a softmax cross entropy cost function (van den Oord et al., 2016). The waveform was nonlinearly transformed with a \(\mu\)-law companding transformation before quantization (van den Oord et al., 2016). The number of bins was equal to the number of sound categories in the original classification task.

Sharpness of a tMTF. The Q factors of tMTFs were calculated as in a previous physiological study (Rodríguez et al., 2010) as follows:

\[
Q = \frac{\text{Centroid}}{\text{Bandwidth}}
\]

where \(\text{Centroid} = \int f_{\text{sr}}(f_\text{m})df_{\text{sr}}\).
where \( f_m \) and \( r(f_m) \) denote the AM rate and tMTF, respectively. Integration was calculated with the trapezoidal rule. Q factors were calculated only in units with a band-pass tMTF.

Statistical analysis. Spearman’s rank correlation coefficients were calculated with the recognition performance and the cascade similarity. The sample size was 100 when comparing them in relation to optimization progress and 39 when comparing them across different model architectures.

Data availability. The datasets used for the training and validation of the model are available from the cited studies (Garofolo et al., 1993; Piczak, 2015). The model architecture is available in Table 1. Source codes for training, evaluation, and physiology of DNNs are available at https://github.com/cycentum/cascaded-am-tuning-for-sound-recognition. Trained models and recorded activities are available at https://doi.org/10.6084/m9.figshare.7914611.

Results

Functional model of the auditory system

The DNN was trained to classify raw sound data (i.e., amplitude waveforms) of nonhuman natural sounds consisting of animal vocalizations and environmental sounds. Therefore, the model covers the entire range of auditory processes from the stage in the ear to the final recognition (Fig. 2). This makes our model suitable for explaining the entire cascade of the auditory system with as few assumptions as possible. This is in contrast to typical auditory studies, which assume frequency-decomposed inputs such as spectrograms. The classification accuracy of the optimized DNN was 45.1% (Fig. 3). We confirmed that a deep cascade is necessary to achieve high classification accuracy (Fig. 4). Although the classification accuracy was not as good as that reported in other studies (Aytar et al., 2016), this difference in
performance is reasonable when we consider that the previous studies used much longer sound segments than ours.

**Emerging tuning to AM rate**

To enable a direct comparison of our DNN and the auditory system, we simulated the experimental approaches of typical neurophysiological studies. Specifically, we conducted “single-unit recording” for each unit in the DNN while presenting a sinusoidally amplitude-modulated sound stimulus (Fig. 5a, b). A single unit responded differently to stimuli with different AM rates (Fig. 5c shows examples). We characterized the tuning of the units’ activities to AM rate in terms of temporal and rate coding with tMTF and rMTF (Joris et al., 2004), namely the synchrony and the average activity as functions of the AM rate, respectively (Fig. 5d).

Figure 6a shows MTFs of representative units in the first, fifth, ninth, and 13th layers. As in typical physiological experiments, we classified the MTFs into low-pass, band-pass, high-pass, or flat types according to certain criteria. Most units exhibited low-pass, band-pass, or flat MTFs (Fig. 6b). All of the MTFs in the first layer were flat, indicating that the first layer did not tune to AM rates. In the fifth layer, units with low-pass or band-pass tMTFs appeared and a very small number of units with low-pass rMTFs were observed. In the ninth and higher layers, the tMTF magnitude generally increased and the number of units with low-pass or band-pass rMTFs also increased. Heat maps of all tMTFs normalized by their peaks reveal a downward shift of the distribution of the preferred AM rates from the fifth layer to the highest layer and distinct tuning in the rMTFs appearing in the ninth layer and above (Fig. 6c).

**Comparison with the auditory system**

As in typical neurophysiological studies, the MTF of a unit was characterized by its BMF, the AM rate at which a neuron exhibits the largest synchrony or average activity, and its UCF, the AM rate at which the synchrony or average activity starts to decrease. The BMF and UCF of temporal and rate coding are denoted tBMF/tUCF and rBMF/rUCF, respectively. In the first and second layers, no BMFs or UCFs were definable because all MTFs were flat (Fig. 7a, b). In the third and fourth layers, some units exhibited definable TBMFs and TUCFs, but no rBMFs or rUCFs were definable. In the fifth layer, the tBMFs and tUCFs appeared to be high and a small number of units exhibited definable rBMFs and rUCFs. When ascending the layer cascade from the fifth layer, the mode tBMF/tUCF decreased and the number of units with definable rBMFs/rUCFs increased. In summary, the distributions of
the tBMFs and tUCFs shifted toward lower AM rates when ascending from the middle to the high layers (Fig. 7a, left) and the units that code AM rate by their average activities appear only in the higher layers (Fig. 7a, right, 7b).

The transformation of the BMF/UCF distributions reminds us of the well known characteristics of the auditory pathway, namely the decrease in synchronizing AM rate and the time-to-rate conversion of AM coding (Joris et al., 2004; Sharpee et al., 2011). Figure 7c depicts the distributions of BMFs and UCFs in the auditory system by combining previously reported distributions for each of the seven brain regions: ANs (Joris and Yin, 1992; Rhode and Greenberg, 1994), the CN (Frisina et al., 1990; Rhode and Greenberg, 1994; Zhao and Liang, 1995; Joris and Smith, 1998; Joris and Yin, 1998), the SOC (Joris and Yin, 1998; Kuwada and Batra, 1999), the nuclei of the lateral lemniscus (NLL) (Huffman et al., 1998; Batra, 2006; Zhang and Kelly, 2006), the inferior colliculus (IC) (Müller-Preuss, 1986; Langner and Schreiner, 1988; Batra et al., 1989; Condon et al., 1996; Krishna and Semple, 2000), the medial geniculate body (MGB) (Preuss and Müller-Preuss, 1990; Lu et al., 2001; Bartlett and Wang, 2007), and the auditory cortex (AC) (Müller-Preuss, 1986; Schreiner and Urban, 1988; Bieser and Müller-Preuss, 1996; Schulze and Langner, 1997; Eggermont, 1998; Lu and Wang, 2000; Liang et al., 2002; Scott et al., 2011; Yin et al., 2011). In the peripheral regions, the tBMFs and tUCFs cluster around high AM rates and, as they ascend toward the central region, the mode rates decrease. rBMFs are only reported in the NLL or above and rUCFs are reported in the SOC or above. This meta-analysis suggests that the distributions of the BMF and UCF in the DNN and those in the auditory system are qualitatively similar.

Next, we compared those distributions quantitatively. For each tBMF, tUCF, rBMF, and rUCF, we calculated the similarity between the distribution in each layer of the DNN and the distribution in each region in the auditory system (Fig. 8a) and averaged them to yield the layer–region pairwise similarity (Fig. 8b). Pairs consisting of a DNN layer and a brain region with a large
similarity appeared in the diagonal direction, indicating that lower, middle, and higher DNN layers are similar to the peripheral, middle, and central brain regions, respectively. This similarity of the entire cascade is more clearly observed if we normalize the pairwise similarity by the maximum value in each brain region (Fig. 8c).

Relationship with optimization
The similarity of the entire cascade could be due to the convolutional architecture inherent to the DNN (Saxe et al., 2011) or to optimization for sound recognition. To test these possibilities, we measured the MTFs in the DNN before and during optimization. Before optimization, no unit exhibited clear selectivity in regard to AM rate and there was no transformation of the MTFs across layers (Fig. 9a, left).

As the optimization progressed, the classification accuracy increased as expected (Fig. 9b, top). Auditory-system-like AM tuning gradually emerged in parallel (Fig. 9a). We evaluated the similarity over all the cascades by measuring the degree of diagonality of the pairwise similarity matrix (Fig. 10) and we refer to this as the cascade similarity. A large cascade similarity value indicates that, in the pairwise similarity matrix, cells around a diagonal line exhibit a large similarity and cells around the top left and bottom right corners exhibit a small similarity. The cascade similarity increased as the optimization progressed (Fig. 9b, bottom) and correlated very well with the classification accuracy (Spearman’s rank correlation coefficient $= 0.84, p = 8.57 \times 10^{-28}, n = 100$). The results indicate that the AM representation in the DNN emerged during the optimization.

Because the classification accuracy of a DNN generally depends on its architecture (Bergstra and Bengio, 2012; Bergstra et al., 2013), so could its cascade similarity (Yamins et al., 2014; Kell et al., 2018). We trained DNNs with various architectures and examined them using the same physiological analysis. The classification accuracy of these DNNs varied between 28.2% and 45.1%. The patterns of the layer–region pairwise similarity also varied among the architectures (Fig. 11a) and the cascade similarity correlated with the classification accuracy (Fig. 11b; $p = 0.51, p = 8.08 \times 10^{-4}, n = 39$). The results indicate that AM representation in better-recognizing DNNs have a greater similarity to that in the auditory system. The similarity to the auditory system correlated with the classification accuracy across both different model parameters and different architectures, which suggests that the auditory AM representation is strongly related to task optimization but not to the convolutional operation alone.

Different factors for different regions
The development of the layer–region pairwise similarity during optimization indicates that an auditory-system-like AM representation is initially exhibited only in the lower layers and that, as the optimization progresses, it first emerges in the upper layers and then in the middle layers (Fig. 9a). This pattern was more clearly seen when we calculated the similarity to the auditory system in each layer, which we refer to as layerwise similarity (Figs. 9c, 10). The results imply that multiple factors can underlie these across-layer differences in the developmental pattern. To isolate the possible factors in each region, we conducted three control experiments expecting to see different degrees of similarity emerge in different layers depending on the control conditions.

The first two control experiments tested the effect of the data structure. It has been shown that a DNN is capable of learning the input–output correspondence even when trained on data with random category labels or data without natural statistics (Zhang et al., 2017). Under the first condition, the input–output correspondence was destroyed by shuffling the category labels. Under the second condition, the structure of the input waveform was destroyed by shuffling the amplitude values of each waveform. Under this condition, the DNN was able to classify the novel sounds with some accuracy probably because the shuffled waveform retained its overall amplitude distribution, although both the frequency and temporal statistics were completely destroyed. The DNNs trained under these two conditions exhibited an auditory-system-like AM representation in the lower and upper layers, but not in the middle layers (Fig. 12a,b, orange triangles and green squares). When the DNN was trained on shuffled labels, very few units in the
middle layers appeared to exhibit AM tuning (Fig. 12a, left column). When the DNN was trained on shuffled waveforms, units in the middle layers appeared to exhibit some AM rate tuning, but they synchronized with a much higher AM rate than neurons in the auditory system, resulting in the upper layers being similar to the middle brain regions (Fig. 12a, middle column). The results indicate that a midlevel AM representation requires a natural data structure, although low-
level and high-level representations could emerge even by optimization with unnatural data.

The third control experiment examined the effect of the optimization objective. A DNN can be optimized for behaviorally irrelevant objectives such as a waveform following task (Fig. 12c). Animals do not usually follow a stimulus amplitude waveform precisely and the task is also trivial in the sense of signal processing. The AM representations in the middle to upper layers were to some degree similar to those of the middle brain regions, but no layers exhibited an AM representation similar to that of the central brain regions (Fig. 12a,b, red crosses). In the upper layers, only small numbers of tMTFs exhibited clear tuning and the tBMFs and tUCFs were higher than those of the central brain regions and the proper sound–category correspondence. The upper layers exhibited nonmonotonic responses to the input amplitudes in a DNN optimized for the recognition of vocal elements in speech (Fig. 13a).

The speech dataset provided essentially the same conclusions as those obtained with animal and environmental sounds. The layer–region pairwise similarity matrix exhibited a diagonal pattern (Fig. 13b). The lower, middle, and upper layers were similar to the peripheral, middle, and central regions, respectively. The similarity emerged during the optimization (Fig. 13c; Spearman’s rank correlation coefficient = 0.83, \( p = 3.76 \times 10^{-27} \), \( n = 100 \)) and was weak under control conditions (Fig. 13d). The similarities in the DNNs with various architectures correlated with the classification accuracy (Fig. 13c; \( p = 0.33 \), \( p = 3.91 \times 10^{-7} \), \( n = 39 \)). The results indicate that auditory-system-like AM tuning emerged robustly across different datasets.

**Sharpness of the tMTF**

Thus far, we have focused on the BMF and UCF for characterizing the MTF. Another aspect often considered is the sharpness of a tMTF, which is represented by quality factors (Q factors). Here, we calculated the Q factors of the unit tMTFs as in a previous physiological study (Rodríguez et al., 2010). The distribution of Q factors appeared different in different layers and, within a layer, they were confined to a narrow range (Fig. 14). This is demonstrated by the small standard deviations of the distributions (shown on the right in the histograms). Also, in most layers, the Q factors were <1. These results indicate the emergence of broadly tuned tMTFs with a relatively constant sharpness, which is consistent with the Q values in animals reported in previous studies (Ewert and Dau, 2000; Lorenzi et al., 2001; Rodríguez et al., 2010).

**Tuning to acoustic frequency**

We also examined tuning to the AF, which is the most frequently measured characteristic in auditory science (Pickles, 2012). We presented sinusoids with various AFs and amplitudes to the DNN and characterized the single-unit responses with the temporal average of the units’ activities (Fig. 15a). The responses generally increased as the input amplitude increased, but some units in the upper layers exhibited nonmonotonic responses to the input am-
plitude. As in the neurophysiological studies, a unit was characterized by an AF tuning curve, namely the minimum stimulus amplitude that provides a response larger above a certain threshold (Fig. 15a, gray and black lines, 15b). Tuning curves from the first to third layers exhibited many troughs (or local minima). Those around the fifth layer exhibited a small number of major troughs and many minor troughs. The major trough of a unit can be interpreted as exhibiting a band-pass property. The center frequencies of the major troughs of the unit population spanned a wide AF range (Fig. 15b), which may be interpreted as a band-pass filter bank. The tuning curves in higher layers were more complex without clear band-pass-like tunings. The overall results were in contrast to those for the auditory system, where neurons across many regions usually exhibit AF tuning with a relatively

Figure 11. Cascade similarity of DNNs with various architectures correlated with their classification accuracy. a, Heat maps showing the layer–region pairwise similarity sorted in terms of classification accuracy, which is shown at the top of each panel. The top left panel is identical to Figure 8b. Pairwise similarities along a diagonal line appeared larger in DNNs with high classification performance. b, Cascade similarities of DNNs with various architectures plotted against their classification accuracies. A single circle represents a single architecture.
Figure 12. AM representation in DNN with control conditions. 

a, AM representation in a DNN trained on shuffled category labels (left column), on shuffled waveform (middle column), and optimized for the waveform following task (right column). Colored symbols and lines by the panel titles indicate the types of control condition as in b. Other conventions are the same as in Figure 9a. 

b, Layerwise similarity in the control experiments. The similarities under the original condition (yellow diamonds and solid line) are also shown. (Figure legend continues.)
sharp single peak. This property is likely to originate from AF decomposition occurring in the cochlea. We did not explicitly implement the spectral decomposition of the input sound but directly fed raw waveforms to the DNN. The results suggest that AF decomposition in the cochlea may be essential for auditory-system-like AF tuning, but not for auditory-system-like AM tuning.

Discussion
We found that a DNN optimized for natural sound recognition exhibits an AM tuning similar to that of the auditory system throughout the entire cascade of layers. Because our DNN was not designed or trained to reproduce any physiological or anatomical properties of the auditory system, the results should reflect only the nature of the task and the data. Therefore, AM tuning in the auditory system might also emerge during evolution and development via optimization to sound recognition in the real world.

Physiology in a DNN
Although DNNs have explained sensory representation in several modalities (Khaligh-Razavi and Kriegeskorte, 2014; Yamins et al., 2014; Horikawa and Kamitani, 2017; Zhuang et al., 2017; Cueva and Wei, 2018; Kell et al., 2018), to the best of our knowledge, this is the first report of the similarity throughout the entire cascade of sensory processing. This could be realized by single-unit recording, which is a highly general neurophysiological technique, on a DNN performing sound recognition from a raw sound waveform. The generality of single-unit recording enabled us to take advantage of the long-accumulated neurophysiological knowledge of AM representation in a variety of brain regions and modeling the entire auditory process enabled us to map all the stages of the process to the corresponding brain regions. Although this study focused on AM representation, the neural representation of any domains of stimulus parameters can be explored using the same paradigm as long as the property of interest can be measured with single-unit recording.

From the perspective of machine learning, our results suggest the effectiveness of analyzing DNNs with physiological methods. To date, various methods have been proposed for analyzing representation in a DNN (Montavon et al., 2018). Most of them rely on the differentiability of the DNN and use backpropagation to estimate the optimal input for each unit assuming such an input exists. By contrast, there is a long history regarding the development of a physiological method for explaining biological neurons, to which backpropagation cannot be applied (Sharpee et al., 2011). The success of our paradigm opens up the future possibility of using well-established physiological methods to explore the stimulus representation of a DNN and other complex machine learning models.

Table 2. Major factors for AM representation in different regions

| Regions   | Major factor                  |
|-----------|-------------------------------|
| Higher    | Optimization objective        |
| Middle    | Data naturalness              |
| Lower     | Cascading architecture        |

AM representation in different regions
The result showing that there was little tuning in the peripheral region may be due to the architecture in which simple operations are cascaded. Computing the AM rate requires at least envelope extraction and the frequency decomposition of the envelope. A small number of peripheral brain regions are probably incapable of such nontrivial computation.

Midlevel neural processing may be a necessary step if the brain is to form a proper stimulus representation for further processes in various tasks. Because lower layers do not tune to an AM rate, the middle layers are effectively the first layers that process AM signals. It is reasonable to think that the first stage of the data process is affected by the data structure and is critical for later recognition.

A higher representation may be directly used for the final recognition process. In other words, whatever the stimulus representation is, the role of the central auditory regions is to derive appropriate outputs for the specific task.

Reduction in temporal resolution
Both of the prominent characteristics of auditory AM coding, namely a decrease in synchronizing AM rate and time-to-rate conversion, involve a reduction in a signal’s temporal resolution. Why is such a scheme beneficial for sound recognition? With our model, as in a typical recognition task with a DNN, the final output at each time frame is the category label assigned to the unit with the maximum activation at the time in the classification layer (the layer above the 13th layer). If the units synchronize with a fast AM, then the output category will be temporally unstable. Conversely, if the activation of a classification unit is large all the time, then the DNN will output a constant category over time. The latter case is preferable for the classification of sounds of a reasonable duration.

Strictly speaking, by avoiding the pooling operation that is often included in typical DNNs, the layers in our DNN do not necessarily down-sample the input. However, even without pooling, it is still possible that successive integration by convolution and half-wave rectification could bias the DNN toward implicitly extracting relatively clean temporal properties such as envelopes. From the result of the waveform following experiment (Fig. 13d), at least we can conclude that proper setting for optimization is necessary for down-sampling properties to emerge in the DNN. Although we avoided making explicit assumptions on DNN parameters by learning them for sound recognition, the architecture of the DNNs with cascaded nonlinearity could induce some significant biases regarding the temporal properties of the extracted signals. Future experiments without half-wave rectification or convolution may reveal the effect of these operations.

Sharpness of a tMTF
In neurophysiological and psychophysical studies, tMTFs have also been characterized by their sharpness. One study has shown that most of the neurons recorded in the central nucleus of the IC exhibit Q factors between 0.5 and 1.5 (see supplemental figure S3A in Rodríguez et al., 2010). Interestingly, layers 7–9 in our DNN, which exhibited IC-like sharpness distributions, were also similar to the IC in terms of BMF/UCF distributions (Fig. 8c). Although unitwise Q factors may not be directly comparable to those of psychophysical tMTFs, most Q values in our DNN were <1 and thus fall in the range suggested by psychophysical studies (Ewert and Dau, 2000; Lorenzi et al., 2001). These results suggest that the broad tuning to the AM rate, which is seen in the auditory system, may be effective for natural sound recognition.
AF tuning

Unlike neurons in the auditory system, our DNN did not exhibit sharp single troughs in the AF tuning curves, although some other studies have reported auditory-like AF tuning emerging in a DNN with a different architecture from ours (Hoshen et al., 2015; Terashima and Furukawa, 2018). In the auditory system, the AF tuning of a neuron depends largely on the mechanical and physical properties of the cochlea (Pickles, 2012). Some architectural constraints might be necessary to induce similarity in the auditory system in the AF domain. By not using a spectrogram as an input, the use of the spectral information such as harmonics for sound recognition may become more direct, which may lead to the complex spectral selectivity shown in our AF tuning curves. The application of a similar convolutional DNN to the temporal and spectral dimensions of a spectrogram might result in more organized “spectrotemporal” tunings similar to those in the auditory system, although an investigation of what determines the shape of an AF tuning curve in a DNN is beyond the scope of this study.

Several other computational studies have tried to explain auditory AM coding by using models with anatomical and physiological assumptions, including AF decomposition in a cochlea (Pešán et al., 2015; McWalter and Dau, 2017; Khatami and Es-
In contrast, our results indicate that auditory-like AM coding emerges even without cochlear AF decomposition. Sharp AF tunings are probably unnecessary to obtain an effective AM representation for natural sound recognition.

**Potential impact on plasticity studies**

In this study, we analogized the auditory system with the optimized DNN. It is difficult to clearly identify the biological counterparts of the DNN optimization process. They probably include a mixture of the effects of short-term plasticity and long-time evolution over generations. Although it may be impractical to experimentally manipulate the long-time evolution in humans, studies with various AM detection or discrimination tasks in humans suggest that the responses of central auditory neurons to AM cues are plastic and that practice may modify the AM processing circuitry (Fitzgerald and Wright, 2005, 2011; Rosen et al., 2012; Sabin et al., 2012; Caras and Sanes, 2015; Joosten et al., 2016). It may be interesting future work to use a DNN model like ours to explore the mechanisms underlying such short-term plasticity.

**References**

Aytar Y, Vondrick C, Torralba A (2016) SoundNet: learning sound representations from unlabeled video. Adv Neural Inf Process Syst 29:892–900.
Bacon SP, Grantham DW (1989) Modulation masking: Effects of modulation frequency, depth, and phase. J Acoust Soc Am 85:2575–2580.
Bartlett EL, Wang X (2007) Neural representations of temporally modulated signals in the auditory thalamus of awake primates. J Neurophysiol 97:1005–1017.
Batra R (2006) Responses of neurons in the ventral nucleus of the lateral lemniscus to sinusoidally amplitude modulated tones. J Neurophysiol 96:2388–2398.
Batra R, Kuwada S, Stanford TR (1989) Temporal coding of envelopes and their interaural delays in the inferior colliculus of the unanesthetized rabbit. J Neurophysiol 61:257–268.
McWalter R, Dau T (2017) Cascaded amplitude modulations in sound texture perception. Front Neurosci 11:485.

Mlynarski W, McDermott JHH (2017) Learning mid-level auditory codes from natural sound statistics. Neural Comput 30:631–669.

Montavon G, Samek W, Müller K-R (2018) Methods for interpreting and understanding deep neural networks. Digit Signal Process 73:1–15.

Müller-Pess P (1986) On the mechanisms of call coding through auditory neurons in the squirrel monkey. Eur Arch Psychiatry Neurol Sci 236:50–55.

Olshausen BA, Field DJ (1996) Emergence of simple-cell receptive field properties by learning a sparse code for natural images. Nature 381:607–609.

Pešan J, Burget L, Hermansky H, Vesely K (2015) DNN derived filters for processing of modulation spectrum of speech. Annu Conf Int Speech Commun Assoc 16:1908–1911.

Pickles JO (2012) An introduction to the physiology of hearing. Available at: https://books.google.co.jp/books?id=8LIumEACAAJ&source=gbs_book_other_versions. Accessed August 3, 2018.

Piczak KJ (2015) ESC: Dataset for Environmental Sound Classification. ACM Int Conf Multimed 23:1015–1018.

Preuss A, Müller-Pess P (1990) Processing of amplitude modulated sounds in the medial geniculate body of squirrel monkeys. Exp Brain Res 79:207–211.

Rhode WS, Greenberg S (1994) Encoding of amplitude modulation in the cochlear nucleus of the cat. J Neurophysiol 71:1797–1825.

Rodriguez FA, Chen C, Read HL, Escabi MA (2010) Neural modulation tuning characteristics scale to efficiently encode natural sound statistics. J Neurosci 30:15969–15980.

Rosen MJ, Sarro EC, Kelly JB, Sanes DH (2012) Diminished behavioral and neural sensitivity to sound modulation is associated with moderate developmental hearing loss. PLoS One 7:e41514.

Sabin AT, Eddins DA, Wright BA (2012) Perceptual learning evidence for tuning to spectrotemporal modulation in the human auditory system. J Neurosci 32:6542–6549.

Saxe A, Koh PW, Chen Z, Bhand M, Suresh B, Ng AY (2011) On random weights and unsupervised feature learning. Int Conf Mach Learn 28:1089–1096.

Schmidhuber J (2015) Deep learning in neural networks: an overview. Neural Netw 61:85–117.

Schreiner CE, Urban J (1998) Representation of amplitude modulation in the auditory cortex of the cat. II. Comparison between cortical fields. Hear Res 32:49–63.

Schulze H, Langner G (1997) Periodicity coding in the primary auditory cortex of the mongolian gerbil (Merionesunguiculatus): two different coding strategies for pitch and rhythm? J Comp Physiol A Neuroethol Sens Neural Behav Physiol 181:651–663.

Scott BH, Malone BJ, Semple MN (2011) Transformation of temporal processing across auditory cortex of awake macaques. J Neurophysiol 105:712–730.

Shannon RV, Zeng FG, Kamath V, Wygonski J, Ekfeld M (1995) Speech recognition with primarily temporal cues. Science 270:303–304.

Sharpee TO, Atencio CA, Schreiner CE (2011) Hierarchical representations in the auditory cortex. Curr Opin Neurobiol 21:761–767.

Smith EC, Lewicki MS (2006) Efficient auditory coding. Nature 439:978–982.

Terashima H, Furukawa S (2018) Reconsidering the efficient coding model of the auditory periphery under reverberations. Annu MidWinter Meet Assoc Res Otolaryngol 41:505.

Terashima H, Okada M (2012) The topographic unsupervised learning of natural sounds in the auditory cortex. Adv Neural Inf Process Syst 25:2312–2320.

van den Oord A, Dieleman S, Zen H, Vinyals O, Graves A, Kalchbrenner N, Senior A, Kavukcuoglu K (2016) WaveNet: a generative model for raw audio. Available at: https://arxiv.org/abs/1609.03499. Accessed: May 22, 2019.

Varnet L, Ortiz-Barajas MC, Erra RG, Gervain J, Lorenzi C (2017) A cross-linguistic study of speech modulation spectra. J Acoust Soc Am 142:1976–1989.

Viereimster NF (1979) Temporal modulation transfer functions based upon modulation thresholds. J Acoust Soc Am 66:1364–1380.

Yamins DL, Hong H, Cadieu CF, Solomon EA, Seibert D, DiCarlo JJ (2014) Performance-optimized hierarchical models predict neural responses in higher visual cortex. Proc Natl Acad Sci U S A 111:8619–8624.

Yin P, Johnson JS, O’Connor KN, Sutter ML (2011) Coding of amplitude modulation in primary auditory cortex. J Neurophysiol 105:582–600.

Yosinski J, Clune J, Bengio Y, Lipson H (2014) How transferable are features in deep neural networks? Adv Neural Inf Process Syst 27:3320–3328.

Zhang C, Bengio S, Hardt M, Recht B, Vinyals O (2017) Understanding deep learning requires rethinking generalization. Int Conf Learn Represent 5:1–15.

Zhang H, Kelly JB (2003) Glutamatergic and GABAergic regulation of neural responses in inferior colliculus to amplitude-modulated sounds. J Neurophysiol 90:477–490.

Zhang H, Kelly JB (2006) Responses of neurons in the rat’s ventral nucleus of the lateral lemniscus to amplitude-modulated tones. J Neurophysiol 96:2905–2914.

Zhao HB, Liang ZA (1995) Processing of modulation frequency in the dorsal cochlear nucleus of the guinea pig: amplitude modulated tones. Hear Res 82:244–256.

Zhuang C, Kubilius J, Hartmann MJ, Yamins DL (2017) Toward goal-driven neural network models for the rodent whisker-trigeminal system. Adv Neural Inf Process Syst 30:2552–2562.