Title: Quantifiable breathing pattern components can predict asthma control: an observational cross-sectional study

Authors: Panagiotis Sakkatos¹, Anne Bruton¹ and Anna Barney²

¹School of Health Sciences, University of Southampton, UK

²Institute for Sound and Vibration Research, University of Southampton, UK

Corresponding author: Dr Panagiotis Sakkatos; Email: sakkatosp@yahoo.gr
Abstract

Background: Breathing pattern disorders are frequently reported in uncontrolled asthma. At present, this is primarily assessed by questionnaires, which are subjective. Objective measures of breathing pattern components can provide additional useful information about asthma control. This study examined whether respiratory timing parameters and thoracoabdominal (TA) motion measures could predict and classify levels of asthma control. Methods: 122 asthma patients at STEP 2-5 GINA asthma medication were enrolled. Asthma control was determined by the Asthma Control Questionnaire (ACQ7-item) and patients divided into ‘well controlled’ or ‘uncontrolled’ groups. Breathing pattern components (respiratory rate (RR), ratio of inspiration duration to expiration duration (Ti/Te), ratio of ribcage amplitude over abdominal amplitude during expiration phase (RCampe/ABampe), were measured using Structured Light Plethysmography (SLP) in a sitting position for 5-minutes. Breath-by-breath analysis was performed to extract mean values and within-subject variability (measured by the Coefficient of Variance (CoV%). Binary multiple logistic regression was used to test whether breathing pattern components are predictive of asthma control. A post-hoc analysis determined the discriminant accuracy of any statistically significant predictive model. Results: Fifty-nine out of 122 asthma patients had an ACQ7-item < 0.75 (well-controlled asthma) with the rest being uncontrolled (n= 63). The absolute mean values of breathing pattern components did not predict asthma control ($R^2 = 0.09$) with only mean RR being a significant predictor ($p < 0.01$). The CoV% of the examined breathing components did predict asthma control ($R^2 = 0.45$) with all predictors having significant odds ratios ($p < 0.01$). The ROC curve showed that cut-off points > 7.40% for the COV% of the RR, > 21.66% for the CoV% of Ti/Te and > 18.78% for the CoV% of RCampe/ABampe indicated uncontrolled asthma. Conclusion: The within-subject variability of timing parameters and TA motion can be used to predict asthma control. Higher breathing pattern variability was associated with uncontrolled asthma suggesting that irregular resting breathing is an indicator of poor asthma control.
Keywords: Breathing patterns, within-subject variability, asthma control, Structured Light Plethysmography
Introduction

Breathing pattern disorders (also known as dysfunctional breathing) are commonly reported in patients with uncontrolled asthma, even though their relationship (causal or coincidental) has not been clearly determined yet (1,2). Dysfunctional breathing has been characterised as a change in the biomechanical and physiological components of breathing, resulting in intermittent or chronic respiratory and non-respiratory symptoms, which worsens asthma patients’ quality of life (3). The most commonly reported respiratory symptoms of dysfunctional breathing are predominant upper thoracic breathing, asynchrony between ribcage and abdominal motion, breathlessness, chest tightness, wheezing and deep sighing (4). However, most of these have been described subjectively through clinicians’ observations or using symptom questionnaires, such as the Nijmegen Questionnaire (NQ) (5). The use of the NQ in this way has been criticised due to its reliance on patients’ perceptions, and its subjectivity (6,7). Objective measures of quantifiable breathing pattern components are needed to increase our understanding of the complex relationship between breathing patterns, symptoms and asthma control.

Breathing pattern comprises components of volume, timing and thoracoabdominal (TA) movements (8). Breathing pattern components, such as tidal volume (Vt), timing parameters (inspiration and expiration duration or their ratio, respiratory rate (RR)) and TA motion, can now be measured non-invasively without requiring patients’ cooperation as traditional lung function tests do (9,10).

Although changes in some of these quantifiable breathing pattern components among asthma patients have been previously reported (11), any relationship of them with different levels of asthma control have not been examined thoroughly. This may lead to a current lack of use of quantifiable breathing pattern components in the evaluation process of asthma control. A positive weak correlation (r=0.33) has been previously reported between TA asynchrony, as measured using Respiratory Inductive Plethysmography (RIP), and Asthma Control Questionnaire (ACQ7-item) (12). In addition, Raoufy et al. (2016) has previously reported that within-subject variability of Vt and
breath cycle duration as measured by the RIP, could differentiate uncontrolled asthma patients (n=10) from patients with well-controlled asthma (n=10) as determined by the presence of asthma symptoms. However, there is still a lack of information about the use of other quantifiable breathing pattern components to indicate levels of asthma control.

To date, traditional lung function tests primarily provide information about airway calibre and lung volume during single forced expiratory maneuvers. Dynamic breathing pattern measures during resting breathing over time may provide additional information to increase our understanding of their physiological role in the evaluation process of asthma control. Thus, the aim of this study was to establish whether respiratory timing parameters and/or respiratory TA movements measured using Structured Light Plethysmography (SLP) during resting breathing, could predict asthma control.

**Methods**

This observational cross-sectional study recruited 122 adult asthma patients with a range of asthma severity from a difficult-to-treat outpatient clinic at the University Hospital Southampton and from staff and students at the University of Southampton. Individuals with a medical diagnosis of asthma without any other chronic respiratory disease or any upper respiratory tract infection on the day of data collection were eligible for this study. Levels of asthma control were determined by the ACQ7-item, and cut-off points < 0.75 and > 1.50 were used to define well-controlled and uncontrolled asthma respectively. Asthma patients with partially-controlled asthma (ACQ7-item scores between 0.75 and 1.50) were not included in this study. All participants were between STEP 2 and STEP 5 asthma medication according to GINA guidelines (14).

After obtaining informed consent, participants’ demographic data and medication history were collected. Asthma medication data was used to determine asthma severity. Participants’ breathing pattern components were recorded during resting breathing in a seated position and then spirometry (Vitalograph) was performed to evaluate lung function.
Breathing pattern components were recorded using the SLP (Thora-3Di™, Pneumacare Ltd) according to manufacturers’ guidelines (15). This is a non-invasive motion-analysis recording system. It comprises a contactless device which projects a grid pattern of light onto an individual’s chest wall covering the area between the clavicles and the umbilicus. The distortion of the grid pattern intersection points caused by the displacement of the anterior surface of the chest wall is recorded by two digital cameras. The two digital cameras are attached on the SLP which generates a time-varying output trace. The manufacturer’s own software did not allow direct breath-by-breath estimations of ribcage and abdominal amplitudes (RCampe and ABampe). Thus, an automatic peak detection algorithm written in Matlab code and used in our previous research (16) was used to obtain values of breathing pattern components during a breath by breath analysis of SLP’s output trace.

The automatic algorithm identified local minima and maxima of the inspiration phase for each breath cycle. The RR was defined as the number of complete breath cycles in one minute and the inspiratory/expiratory phase ratio (Ti/Te) was defined as the proportionality between inspiratory and expiratory phases. The inspiratory time (Ti) was calculated as the time between a minimum in the sum SLP output trace and the next peak. The expiratory time (Te) was calculated as the time between a peak and the next minimum. The ribcage and abdominal amplitudes (RCampe and ABampe) were defined as the vertical distances between a trough and the next peak on the SLP’s output as derived from the different SLP’s traces used to record the motion of the ribcage and abdomen separately. The within-subject variability of the breathing pattern components was calculated as the Coefficient of Variance expressed as a percentage (CoV%).

The patients’ breathing pattern components were recorded for 5 minutes at the sitting position. The participants were requested to stay still and quiet during the whole recording procedure. This was to minimise external body movement artefacts on the SLP’s output trace as this could bias values of breathing pattern components during data extraction. When patients were ready to be recorded,
they were falsely informed about the start of breathing pattern recording. The actual recording time
started one minute after the initial notification. This was to eliminate any impact of the patients’
awareness on breathing pattern measurements whilst recording natural behavior of their breathing.

Descriptive statistics were used to summarise demographic data and lung function measurements.
Comparisons of the breathing pattern components between well-controlled and uncontrolled
asthma groups were made using the Mann-Whitney U test (significance level p < 0.01) as normal
distribution of the data was not found. Multiple binary logistic regression, using the forced method,
was performed to predict uncontrolled asthma (ACQ7-item > 1.50). Two regression models were
applied, one using absolute mean values of RR, Ti/Te and RCampe/ABampe as predictors. The other
one involved the within-subject variability measures (Cov%). Both regression models met the
assumption of multicollinearity (Variance Inflation Factor < 10). When all predictors of a regression
model significantly predicted uncontrolled asthma, a post-hoc analysis using a Receiver Operating
Characteristic curve (ROC) was used to identify cut-off points for changes in breathing pattern
components distinguishing well-controlled and uncontrolled asthma.

Results

One hundred twenty two adult asthma patients (75 females) were recruited and completed the
study (mean age (sd) 44.75 years (15.98 years). Sixty-three participants had an ACQ score of > 1.5
(uncontrolled asthma), whereas 59 participants scored < 0.75 (well-controlled asthma). Thirty-three
participants had mild asthma (STEP 2 on GINA asthma medication), with 29 of these being in the
well-controlled group while the rest of them had moderate-to-severe asthma (STEP 3, 4 and 5 on
GINA asthma medication). There were similar numbers of males and females in both groups (Table
1). Both groups also had similar average body mass index (BMI). Those in the uncontrolled asthma
group had reduced average lung function compared to the well-controlled asthma group (Table 1).

Although those in the uncontrolled asthma group had significantly higher median RR than those in
the well-controlled group, no significant differences were found for the other absolute mean values
of breathing pattern components (Ti/Te and RCampe/ABampe) (Table 2). On the other hand, the
within-subject variability measures (CoV%) of all the breathing pattern components were found to
be significantly increased in the uncontrolled asthma group compared to the well-controlled group
(Table 2).

When mean values of RR, Ti/Te and RCampe/ABampe were entered into the regression model
asthma control was not predictable with only the beta coefficient of RR being significantly greater
than zero (Table 3). When within subject variability measures (CoV%) of breathing pattern
components were entered into the model, a good fit was found (Table 4). This accounted for 45% of
the variance in the ACQ7-item scores. The beta coefficients of the CoV% of all breathing pattern
components were found to be significantly greater than zero suggesting that increased within-
subject variability of RR, Ti/Te and RCampe/ABampe predicts uncontrolled asthma. A linear
relationship was found between the CoV% of all breathing pattern components and the log of the
ACQ7-item score with no more than 5% of the total cases being considered as influential cases
(standardised residuals > 2) in the specific regression model.

A post-hoc analysis showed that a regression model including the CoV% of breathing pattern
components correctly classified 53 out of 59 patients with ACQ7-item < 0.75. It also correctly
classified 48 out of 63 patients with ACQ7-item > 1.50. The sensitivity and specificity of the
regression model were estimated to be 77.94% and 88.88% respectively with the area under the
ROC being 0.895 (95% CI[0.84, 0.95], sig 0.000, p < 0.01) (Figure 1). Based on individual ROCs for the
CoV% of individual breathing pattern components (Figure 2), a cut-off point > 7.40% for the CoV% of
the RR discriminated well-controlled from uncontrolled asthma. Optimal cut-off points for the CoV%
of Ti/Te and RCampe/ABampe were estimated to be > 21.66% and > 18.96% respectively (Table 5).

Discussion

The study aimed to examine whether respiratory timing parameters and/or respiratory TA
movements could predict and classify levels of asthma control. The within-subject variability of
breathing pattern components, such as RR, Ti/Te and RCampe/ABampe, was found to predict asthma control, but their absolute mean values did not. Based on these findings, the within-subject variability of breathing pattern components is likely to be a better indicator of asthma control than their mean values when measured in a single occasion. This may be because the within-subject variability can efficiently reflect the natural behaviour of tidal breathing over time compared to the absolute mean values of the same respiratory parameters. Therefore, the study’s findings suggest that the regularity of resting breathing can be considered as another physiological marker which reflects levels of asthma control. The importance of measuring the natural behaviour of breathing patterns has been previously highlighted as this may reflect better the adaptability of the respiratory system occurred during symptomatic periods of asthma (17).

On the other hand, the limited variance we found in the absolute mean values of Ti/Te and RCampe/ABampe may have biased the asthma control prediction. Although the RR was found to be a significant predictor of asthma control, there was a lack of a linear relationship between mean RR and asthma control. All these may be attributed to the presence of confounders previously reported in cross-sectional observational study designs (18, 19). Authors’ expect that examples of such confounders could be a postural effect, the patients’ asthma complexity, the underlying patients’ anxiety levels, and an effect of rescue medication usage prior to breathing pattern measurements. Some of these, such as posture and emotions, have been clearly suggested to affect absolute mean values of breathing pattern measurements (18,19, 20), but the impact of asthma complexity and medication usage on breathing patterns is not clear yet.

Respiratory rate is affected by many factors, and so there was no clear separation between the well-controlled and controlled groups for this parameter. Asthma patients frequently have co-existing anxiety which can have an impact on RR (21). There is also a relationship between asthma and obesity (22), and it is well known that BMI can have an impact not only on patients’ asthma control but also on timing components of breathing patterns (23). Although levels of anxiety were not
assessed in our study, our study’s individuals with raised RR and well-controlled asthma were obese (BMI >30 kg/m²). The normal RR found in some individuals of the uncontrolled asthma group is unexplained, but this may have been caused by the use of rescue medication prior to breathing pattern recordings during this study.

Raoufy et al. (2016) have previously reported that the within-subject variability of Vt and breath cycle duration can differentiate patients with well-controlled asthma from those with uncontrolled asthma. Our findings are in agreement with Raoufy et al.’s work despite methodological differences, such as the method used to determine asthma control (National Asthma Education and Prevention program vs ACQ7-item), the breathing pattern recording time (60 minute vs 5 minutes), the recording posture (supine vs sitting) and the equipment used to monitor breathing patterns (SLP vs RIP) at rest.

The optimal time for recording variability within breathing pattern parameters is not known in the literature. We measured within-subject variability over 5 minutes and found this was sufficient for making significant predictions of asthma control using respiratory rate, proportionality of respiratory phases, and TH motion. To the best of authors’ knowledge, the study presented here also provides for a first time specific cut-off points for the within-subject variability of the breathing pattern components, which can be used to differentiate well-controlled from uncontrolled asthma.

However, more research is required to confirm the accuracy of our results in the future. In addition, the different posture selected in our study compared to Raoufy et al. (2016) did not seem to have an impact on the ability of within-subject variability of the breathing pattern components to predict asthma control. However, more research involving different postures, such as supine or standing, is required to check maintenance of the identified association between asthma control and within-subject variability of breathing pattern components.

Some limitations underlie this research. We did not include patients with partially controlled asthma (ACQ7-item score between 0.75 and 1.50) so that ACQ7-item score could be used as a binary
outcome within the recruited sample. A causal or coincidental relationship between within-subject variability and asthma control could not be determined from our findings due to the selected study design. It is not known whether uncontrolled asthma preceded the increased within-subject variability of the breathing pattern components, or vice versa. However, it is assumed that increased within-subject variability in the presence of uncontrolled asthma might be due to physiological, psychological or biomechanical factors as previously observed in the literature (3). In any way, a future prospective cohort study is required to examine the exact nature of the relationship between the changes in quantifiable breathing pattern components and asthma control.

**Conclusion**

The study showed that within-subject variability of timing parameters and THA motion predicts and classifies levels of asthma control, but same results were not found for mean values of them. It is concluded that increased within-subject variability of RR, Ti/Te and RCampe/ABampe is associated with uncontrolled asthma. This sheds a light on the use of stable resting breathing as another important marker of asthma control.

**List of abbreviations**

TA: thoracoabdominal; ACQ7-item: Asthma Control Questionnaire ; RIP: Respiratory Inductive Plethysmography; RR : Respiratory Rate ; Ti/Te : ratio of inspiration phase over expiration phase; RCampe/ABampe: ratio of ribcage amplitude over abdominal amplitude during the expiration phase; SLP: Structured Light Plethysmography; CoV%: Coefficient of Variance expressed in a percentage; DB: Dysfunctional breathing; NQ: Nijmegen Questionnaire; sd: standard deviation; ROC: Receiver Operating Characteristics curve

**Declarations**

**Ethics approval and consent to participate**
The study has been approved by the London-Queen Square Ethics Committee (Rec no: 17/LO/1640; IRAS ID: 230295). All participants provided a written consent form prior to their participation in the study.

Consent for publication

Patients’ anonymous data were agreed to be published for maintaining anonymity and protecting individuals’ health data.

Availability of data and materials

The datasets used and analysed during the current study are available from the corresponding author on reasonable request.

Competing interests

The authors declare that they have no competing interests.

Funding

This research study was funded by British Lung Foundation and Wessex Medical Trust. This study was part of the first author’s PhD work which would not be possible to be completed without the funders’ financial support.

Authors’ contributions:

All authors participated in the developmental phase of this research and the preparation of this paper. The first author was also responsible for collecting and analysing study’s data with the other authors providing their valuable supervision.

Acknowledgements

The authors thank the funders for their financial support of this study through a fellowship. The authors also thank all the participants for their input in this study. Finally, the authors thank Dr Hans...
Michael and Dr Ramesh Kurukullaaratchy for facilitating access to their outpatient clinic at University Hospital Southampton where participants’ recruitment and data collection occur.

Authors’ information:

Panagiotis Sakkatos, PhD, MSc, BSc respiratory physiotherapist; Anne Bruton, Emeritus Professor of Respiratory Rehabilitation, PhD MA (Cantab), MCSP; Anna Barney, Professor of Biomedical Acoustic Engineering PhD, MSc, BSc.

References

1. Agache I, Ciobanu C, Paul G, Rogozea L. Dysfunctional breathing phenotype in adults with asthma-incipense and risk factors. Clin Transl Allergy. 2012;2:8
2. Veidal JM, Jeppegaard M, Sverrild A, Backer V, Porsbjerg C. The impact of dysfunctional breathing on the assessment of asthma control. Respiratory Medicine. 2017;123:3
3. Courtney R. Breathing retraining for dysfunctional breathing in asthma: taking a multidimensional approach. European Respiratory Journals Open Research. 2017; 3:4
4. Baker N, Everard ML. Getting to grips with “dysfunctional breathing”. Paediatric Respiratory Reviews. 2015;16:1
5. Boulding R, Stacey R, Niven Rand Fowler SJ. Dysfunctional breathing: a review of the literature and proposal for classification. European Respiratory Reviews. 2016; 25:141
6. Van Dixhoorn J, Folgering H. The Nijmegen Questionnaire and dysfunctional breathing. European Respiratory Journal Open Research. 2015;1:1
7. Vidotto LS, Carvalho CRF, Harvey A, Jones M. Dysfunctional breathing: what do we know? Jornal Brasileiro de Pneumologia. 2019;45:1
8. Tobin MJ. Breathing pattern analysis. Intensive Care Medicine. 1992;18:4
9. Folke M, Cernerud L, Ekstrom M, Hok B. Critical review of non-invasive respiratory monitoring in medical care. Medical and Biological Engineering and Computing. 2003;41:4
10. Motamedi-Fakhr S, Wilson RC and Iles R. Tidal breathing patterns derived from Structured Light Plethysmography in COPD patients compared with healthy subjects. Medical devices. 2017;10:1
11. Lavorini F, Magni C, Chellini E, Camiciottoli MP, Fontana GA. Different respiratory behaviours disclosed by induced bronchoconstriction in mild asthma patients. Respiratory Physiology & Neurobiology. 2013;189:3
12. Upton J, Brodie D, Beales D, Richardson J, Jack S, Warburton C. Correlation between perceived asthma control and thoraco-abdominal asynchrony in primary care patients diagnosed with asthma. Journal of Asthma. 2012;49:8
13. Raoufy MR, Ghafari T, Darooei R, Nazari M, Mahdaviani SA, Esleinejad AR, Almasnia M, Gharibzadeh S, Mani AR, Hajizadeh S. Classification of asthma based on nonlinear analysis of breathing pattern. PLoS One. 2016;11:1

14. Global Initiative for Asthma Global Strategy for Asthma Management and Prevention. GINA guidelines. 2018. https://ginasthma.org/gina-reports/. Accessed 16 April 2018

15. Motamedi-Fakhr S, Iles R, Barney A, De Boer W, Conlon J, Khalid A, Wilson RC. Evaluation of the agreement of tidal breathing parameters measured simultaneously using pneumotachography and structured light plethysmography. Physiological Reports. 2017;5:3

16. Tehrany R. Speech breathing patterns in health and chronic respiratory disease.

17. Frey U, Maksym G, Suki B. Temporal complexity in clinical manifestations of lung disease. Journal of Applied Physiology. 2011;110:

18. Homma I, Masaoka Y. Breathing rhythms and emotions. Experimental Physiology. 2008;93:9

19. Romei M, Lo Mauro A, D’Angelo MG, Turconi AC, Bresolin N, Pedotti A, Aliverti A. Effects of gender and posture on thoracoabdominal kinematics during quiet breathing in healthy adults. Respiratory Physiology & Neurobiology. 2010;172:3

20. Kaneko H, Horie J. Breathing movements of the chest and abdominal wall in healthy subjects. Respiratory Care. 2012;57:9

21. Ritz T, Meuret AE, Trueba AF, Fritzsche A, Von Leupoldt A. Psychosocial factors and behavioural medicine interventions in asthma. Journal of Consulting and Clinical Psychology. 2013;81:2

22. Boulet LP. Asthma and obesity. Clinical & Experimental Allergy. 2012;43:1

23. Chlif M, Keochkerian D, Choquet D, Vaidie A, Ahmaidi S. Effects of obesity on breathing pattern, ventilatory neural drive and mechanics. Respiratory Physiology & Neurobiology. 2009;168:

### Tables and Figures

**Table 1: Demographic data and lung function measurements of asthma control groups**

| Variable          | Well controlled asthma group (n=59) | Uncontrolled asthma group (n=63) |
|------------------|-------------------------------------|----------------------------------|
| Gender           | 23 males; 36 females                | 24 males; 39 females             |
| Asthma severity  | 29 mild; 30 moderate-to-severe      | 4 mild; 59 moderate-to-severe    |
| Age (years)      | 41.20 ± 17.78                      | 48.06 ± 14.56                   |
| BMI (kg/m²)      | 24.95 ± 3.75                       | 26.49 ± 4.01                    |
| FEV₁predicted (%)| 100.90 ± 18.81                     | 76.06 ± 24.93                   |
| FEV₁/FVC         | 81.91 ± 9.44                       | 74.49 ± 15.28                   |
Table 2: The differences in the breathing pattern components between asthma control groups

| Breathing component | Well-controlled group (n = 59) | Uncontrolled group (n = 63) | Mann-Whitney U | p (1-tailed) |
|---------------------|--------------------------------|----------------------------|----------------|--------------|
| RR (bpm)            | M*** 14.92 | Min-Max** 7.09-21.05 | 17.16 | Min-Max 7.40-32.02 | 1175 | 0.000* |
| Ti/Te               | 0.66 | 0.40-0.90 | 0.68 | 0.40-0.96 | 1689 | 0.385 |
| RCampe/ABampe^      | 1.29 | 0.43-4.20 | 1.33 | 0.37-5.31 | 1798 | 0.729 |
| CoVRR (%)           | 4.79 | 0.00-23.02 | 11.73 | 0.00-29.71 | 655 | 0.000* |
| CovTi/Te (%)        | 19.05 | 10.49-46.11 | 33.22 | 14.28-57.39 | 606 | 0.000* |
| CovRCampe/ABampe^^  | 14.82 | 6.05-24.82 | 26.45 | 7.74-57.62 | 844 | 0.000* |

***M: median value; **Min-Max: minimum and maximum values; * significant result at p < 0.01; ^RCampe/ABampe: Ribcage over abdominal amplitude during expiration phase; ^^ CovRCampe/ABampe: The within-individual variability of ribcage over abdominal amplitude during expiration phase

Table 3: The regression model including mean values of breathing pattern components used to predict uncontrolled asthma

| Predictors          | B (SE) | Lower | Odds Ratio | Upper | p      |
|---------------------|--------|-------|------------|-------|--------|
| RR (bpm)            | 0.16 (0.05) | 1.06  | 1.17       | 1.30  | 0.002* |
| Ti/Te               | 0.10 (1.79) | 0.03  | 1.10       | 37.36 | 0.954  |
| RCampeexp/ABampeexp^ | 0.07 (0.29) | 0.61  | 1.07       | 1.88  | 0.812  |

B: 0.07; R^2: 0.09; R: 0.12; -2LL 157.38; * starred sig. value was found to be significant at p < 0.01
Table 4: The regression model including the CoV% of breathing pattern components used to predict uncontrolled asthma

| Predictors                        | B (SE)  | Lower | Odds Ratio | Upper | p     |
|-----------------------------------|---------|-------|------------|-------|-------|
| CoV_{RR} (%)                      | 0.15 (0.05) | 1.05  | 1.16       | 1.29  | 0.000*|
| CoV_{Ti/Te} (%)                   | 0.10 (0.03) | 1.04  | 1.11       | 1.18  | 0.001*|
| CoV_{RCampus/ABampexp} (%)        | 0.09 (0.05) | 1.05  | 1.11       | 1.17  | 0.005*|

B = 0.07; R² = 0.45; R = 0.59; -2LL = 96.87; * starred values were significant results at p < 0.01;

Figure 1: The ROC curve of the regression model including the CoV% of the examined breathing pattern components.
Figure 2: The different ROC curves for the CoV% of RR (blue line), Ti/Te (red line) and RCampe/ABampe (green line)

Table 5: Optimal cut-off points for the CoV% of each breathing pattern component and estimates of the area under the curve (AUC)

| Breathing component | Optimal cut-off point^ | AUC   | Std error | 95% CI         | p       |
|---------------------|------------------------|-------|-----------|----------------|---------|
| CoV_{RR} (%)        | >7.40                  | 0.824 | 0.039     | 0.747-0.900    | 0.000*  |
| CoV_{Ti/Te} (%)     | >21.66                 | 0.837 | 0.038     | 0.763-0.911    | 0.000*  |
| CoV_{RCampe/ABampe} (%) | >18.78               | 0.773 | 0.044     | 0.686-0.859    | 0.000*  |

^Optimal cut-off points were selected as the closest points from the left corner of the individual ROC curves for the CoV% of each breathing parameter; * significant result was defined at p < 0.01