Mechanical behavior of a soft hydrogel reinforced with three-dimensional printed microfibre scaffolds

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Reinforcing hydrogels with micro-fibre scaffolds obtained by a Melt-Electrospinning Writing (MEW) process has demonstrated great promise for developing tissue engineered (TE) constructs with mechanical properties compatible to native tissues. However, the mechanical performance and reinforcement mechanism of the micro-fibre reinforced hydrogels is not yet fully understood. In this study, FE models, implementing material properties measured experimentally, were used to explore the reinforcement mechanism of fibre-hydrogel composites. First, a continuum FE model based on idealized scaffold geometry was used to capture reinforcement effects related to the suppression of lateral gel expansion by the scaffold, while a second micro-FE model based on micro-CT images of the real construct geometry during compaction captured the effects of load transfer through the scaffold interconnections. Results demonstrate that the reinforcement mechanism at higher scaffold volume fractions was dominated by the load carrying-ability of the fibre scaffold interconnections, which was much higher than expected based on testing scaffolds alone because the hydrogel provides resistance against buckling of the scaffold. We propose that the theoretical understanding presented in this work will assist the design of more effective composite constructs with potential applications in a wide range of TE conditions.

Soft tissues, e.g. articular cartilage or cardiac muscle, are complex composite materials consisting of collagen fibrils reinforcing a cell-containing proteoglycan gel-like matrix1,2. To mimic such natural composite structures, recent studies have highlighted the potential of developing composite constructs composed of hydrogels and fibrous materials3–5. Hydrogels, with their highly hydrated polymer network, can provide the cells an environment that further resembles the natural extracellular matrix (ECM)6, whilst the reinforcing fibres can provide the necessary mechanical properties, close to those of biological tissues7. Preparation of such composite materials usually involves a two-step procedure, i.e. fabrication of the fibre reinforcing scaffold and then crosslinking a gel inside these fibre scaffolds8,9. Electrospinning and wet spinning are commonly used techniques for fibre formation due to their relative simplicity and capability to produce sub-micron diameter fibres9,10. However, their difficulty in manufacturing controlled architectures and three-dimensional (3D) complex geometries compromises cell infiltration11 and seriously limits hydrogel mechanical reinforcement12. Recently, it was demonstrated that with a direct melt electrospinning writing (MEW) process, or melt electrowriting as recently designated13, micro-fibre scaffolds could be fabricated with well-controlled 3D architectures14,15. This electrohydrodynamic process forms fibres from polymer melts to deposit highly defined networks, with fibre diameters within the range of 800 nm16 to 150 µm17.

The inclusion of melt-electrospun scaffolds within hydrogels can be used to improve the mechanical properties of hydrogels and simultaneously modulate their mechanical response. Visser et al. demonstrated that the combination of polycaprolactone (PCL) MEW scaffold with a soft gelatine-methacryloyl (GelMA) hydrogel...
synergistically enhance the compressive properties of the composite hydrogel constructs, while still exhibiting an excellent biological performance\(^1\). This synergistic effect was assumed to be due to the fibres being pulled in tension when the construct was loaded in compression, i.e. a Poisson's effect. This assumption was supported by a relatively simple mathematical model that considered the hydrogel and fibre scaffolds as composed of an idealized geometry and linear elastic materials. Nevertheless, it over-predicted the final stiffness of the composite constructs by one order of magnitude. Further studies using GelMA and GelMA/hyaluronic acid-methacrylamide gels reinforced with similar MEW scaffolds corroborate the same theory, although a different reinforcement level was observed as compared to Visser et al.\(^1\). Despite the great potential of the composite constructs, the reinforcing effect of the MEW scaffold is thus not fully understood. The absence of an adequate framework to explain the observed reinforcement mechanism is limiting the optimisation of these novel designs and is hampering their application. The use of computational methods, that could simulate the mechanical behaviour of these composite constructs, can bring valuable insights into the process that governs the reinforcement mechanism, although, the accuracy of these methods is dependent on the precise definition of the material properties, model geometry and interaction between the composite constituents. Also, the difference in mechanical behaviour between the composite components, i.e. soft hydrogels reinforced with stiffer microfibres, is known to lead to non-linear phenomena, e.g. fibre buckling and structural instabilities, that impact on the reinforcement mechanism\(^2\). Therefore, the aim of the present study was to elucidate the mechanics of the reinforced hydrogel composite through FE simulations. Two different FE models were used. The first is a continuum model representing a schematized hydrogel and scaffold geometry (either individually or combined), to investigate the load carrying capacity of hydrogel and scaffold alone, and the reinforcement mechanism due to the scaffold restricting hydrogel movement in composite constructs. The second is a micro-FE model of the scaffold without and with hydrogel, to investigate the actual (buckled) geometry of the scaffold at different states of compression and the load transfer directly through the interconnections of the scaffold at these stages. By combing the simulation results with the experimental results, material parameters of the composite constituents are derived and the reinforcement mechanism of the fibres can be explained in detail.

**Results**

**Construct fabrication and mechanical characterization.** Figure 1 shows the microstructure of fabricated electrospun scaffolds with different fibre volume fractions. While the accurate fibre placement onto the collector enabled the formation of controlled squared fibre arrangements in two-dimensions (2D) (Fig. 1A–F), some fibre sagging occurred towards the middle of the fibre walls, which was more evident for scaffolds with larger fibre spacings (Fig. 1A–F). This is due to the fact that each scaffold was generated with a single fibre filament drawn continuously, which generated multiple crossing fibres at the square edges. Moreover, the efficient combination of the micro-fibre scaffold within the GelMA hydrogel was confirmed (Fig. 1G). As the fibres were written with melt-extrusion, fibres were mostly fused together, forming a membrane-like wall with occasional openings. Similarly, at crossing points the fibers were fused forming a column-like structure.
A thorough mechanical evaluation of the composite constructs was further performed to evaluate the material properties required for the FE models. Tensile tests on single fibre filaments (Supplementary Fig. S1) revealed an elastic fibre modulus of $363 \pm 21.2 \text{ MPa}$, which is within the range previously reported for melt extruded PCL filaments $^{21,22}$. The compressive properties of the fibre scaffolds alone, GelMA hydrogel alone and respective composites are summarised in Table 1. A compression modulus of up to $E = 387 \pm 34.6 \text{ kPa}$ at $v_f = 7.0\% \pm 0.3\%$ was found for fibre reinforcement constructs, while non-reinforced GelMA constructs exhibited a compressive modulus of $E = 8.2 \pm 0.9 \text{ kPa}$ and PCL scaffolds alone $E = 14.1 \pm 1.9 \text{ kPa}$ at same of $v_f = 7.0\% \pm 0.3\%$.

### Table 1. Measured volume fraction, $v_f$, of the reinforcing fibre scaffold, and compressive modulus, $E$, of the composite construct and its hydrogel matrix and fibre scaffold phase alone. Values are mean $\pm \text{ SD}$.

|                        | Hydrogel | Composite construct |
|------------------------|----------|---------------------|
| Fibre filament spacing, $A$ in mm | 0.8      | 0.6                 |
| Fibre volume fraction, $V_f$ in % | $3 \pm 0.2$| $4 \pm 0.1$          |
| E hydrogel matrix in kPa | $8.2 \pm 0.9$ | $4.2 \pm 0.5$         |
| E fibre scaffold phase in kPa | $8.4 \pm 1.3$ | $122.2 \pm 16.21$     |
| E composite in kPa     | $81.4 \pm 10.3$ | $207.43 \pm 40.1$     |

Figure 2. Overview of modeling workflow for both FE models proposed under uniaxial compression. (A) Experimental analysis of fibre reinforced hydrogels mechanical behavior under uniaxial compression to access material properties and validate numerical predictions. (B) Continuum FE model of idealized composite architecture. Only a quarter of the composite construct was modelled with the reinforcing box scaffolds idealized as thin laminas (defined in a local coordinate system) embedded in a hydrogel matrix. At the fibre scaffold interconnections a truss element was added with its longitudinal axis in the global y-direction. (C) Micro-FE model of the real composite architecture at different deformation levels. Real architecture was accessed at increasing levels of compactation with the use of a micro-compression device, as schematically represented, and a high-resolution CT scanner.

### Finite element analysis.

The workflow of the developed FE modelling methodologies is briefly summarized in Fig. 2. For the continuum FE model an idealized model of the composite construct geometry was first generated and the material properties of each constituent, i.e., hydrogel and fibre scaffold, were determined by fitting a FE model of each constituent to the experimental tests performed on isolated materials. Subsequently, the determined constitutive parameters were implement in the FE model of the composite constructs for various fibre volume fractions which was then compared with the experimental data. For the micro-FE model, the actual construct geometries at different compressive strain levels were used to build the model. The constitutive parameters used in the micro-FE were determined using the methodology detailed in the methods section.

### Continuum FE model.

The two parameters of the Neo-Hookean constitutive model for the hydrogel were obtained by fitting the unreinforced hydrogel FE model to the respective experimental results. Table 2 summarizes the determined coefficients and good agreement between the model results and the experimental stress-strain data was observed (Fig. 3A). A sensitivity analysis revealed that the material behavior showed a strong dependency on the estimated shear modulus ($C_{10}$ parameter). However, even changing the $C_{10}$ parameter by 10%, the behavior fell within the spread of the experimental data.
The fibre scaffolds were idealized as unidirectional thin laminas organized in a box structure, with perfectly parallel micro-fibres that could barely withstand stresses in any direction other than that of the micro-fibres. The interconnections, at box vertices, were idealized as columns, due to the multiple inter-weaving of crossing-fibres (Fig. 2B). Table 2 shows the determined material properties accessed by the tensile tests on single fibres and by fitting results calculated from FE analyses representing an uniaxial compression simulation of a fibre scaffold alone with \( V_f = 3\% \); the results demonstrated that the continuum FE model with the new longitudinal modulus implemented still significantly underestimated the modulus of the higher fibre volume fraction composites, being approximately four times lower than the experimentally measured stiffness for different fibre-volume fraction (Fig. 3C). With the determined material properties, the FE model of the fibre scaffold alone represented well the experimentally measured stiffness for the constructs, e.g. because the scaffold deformation in the presence of the gel is very different from that of the scaffold alone. To further investigate this, the micro-FE model was used.

### Micro-FE model

The micro-FE model was created directly from 3D micro CT reconstructed geometries of both fibre scaffold alone and reinforced gel at compressive strain levels of 0, 15, 30 and 45% (data not shown for 45% strain). Preparation of the reconstructed geometries involved the use of a micro-compression device to apply and maintain strain. Subsequently, reconstructed images were converted to micro-FE models, using a voxel conversion procedure and the construct stiffness in the deformed configuration was determined from a micro-FE analysis. Table 2 summarizes the material properties determined by using the fitting procedure summarized in the Methods section, Micro- FE analysis. While evaluating the deformed geometries and compressive stress distribution of scaffolds alone and scaffolds combined with hydrogel, a clear difference was found (Fig. 4 A, B). In the non-deformed configurations, the maximum stress level was predominantly localized at the top crossing fibre regions for the scaffold alone and more uniformly distributed through the scaffold walls and interconnections for the scaffold combined with hydrogel. The stress distribution within the scaffold alone for the deformed conditions (i.e. 30% strain) showed a totally different behavior compared to the non-deformed condition. Stress was clearly localized on the few unbuckled interconnections, while the scaffold walls remained more or less unloaded. In contrast, in the scaffold combined with hydrogel the fibre walls and especially the interconnections remained straight even at larger strains. Moreover, differences in deformation between scaffold alone and scaffold embedded in the hydrogel matrix were consistent with the measured stress-strain response (Fig. S2). For the scaffolds

| Component     | Material     | Material properties | Constitutive material properties |
|---------------|--------------|---------------------|---------------------------------|
| Continuum FE  | Hydrogel matrix | GelMA Neo Hookean hyperelastic C10 | \( C_{33} = 0.00135 \) MPa; \( D_1 = 30 \) MPa \(^{-1}\) |
| Fibre scaffold | PCL          | Linear elastic orthotropic membranes | \( E_1 = 182 \) MPa; \( E_2 = 0.06 \) MPa; \( \nu_{12} = 0.43; G_{12} = 0.88 \) MPa; \( G_{13} = 0.91 \) MPa; \( G_{23} = 1 \times 10^{-7} \) MPa |
| Interconnections | Linear elastic | E int = 3 MPa | |

Table 2. Determined constitutive material parameters for the hydrogel matrix and for the fibre scaffold used for the numerical analysis. Membrane properties were defined according to the local coordinate system (see Fig. 2B).
alone stress is approximately linear up to 15% falling gradually thereafter, while for composite constructs stress is reasonably linear up until larger strains, ≈30 and 45%.

When calculating the stiffness for the deformed scaffolds shapes based on the micro-FE analyses (Fig. 4C), it can be seen that the scaffolds alone have a very low stiffness but when combined with hydrogel their stiffness increases up to 47 fold, caused mostly by prevention of scaffold structural buckling. Also, we observed that the stiffnesses at 30% strain were higher than at 0% strain (i.e. non-deformed), and that the reinforced constructs with higher volume fraction had an approximately 1.5 fold increase in stiffness. This suggested a strong dependence of the interconnections’ load transfer on the reinforcing mechanism. Therefore, the stiffness of reinforced constructs predicted using the continuum FE model and material properties of the fibre scaffold interconnections assessed in a non-buckled versus buckled status for various fibre-fractions were compared (Fig. 4D). The non-buckled interconnections stiffness (E_{non buckled intercom} = 24 MPa) were determined from the composite scaffolds (V_f = 3%) where no significant buckling of the intersections was observed (Figs 4B and S2). This value is still considerable less than the material properties for the PCL fibres (363 ± 21.2 MPa), which likely is due to the fact that the melted contact area between stacked fibres can be much smaller than the cross-sectional area of the fibres.
Figure 4. Micro-FE model results. (A) Comparison of loaded regions between the A) fibre scaffold and the (B) reinforced hydrogel with a volume fraction of 3% and 7%. Loaded regions are represented as compression stress and were determined by micro-FE analysis on non-deformed and deformed real geometries. Stress is in MPa. (C) Stiffness predicted from micro-FE analysis. Stiffness was relativized by dividing each value by the maximum value. (D) Comparison of the predicted and experimental stiffnesses for the reinforced constructs (E_reinf) with buckled and non-buckled interconnections stiffness using the continuum FE model. Interconnections material properties were re-fitted to the composite construct with a \( v_f = 3\% \), where no buckling was observed.

(Fig. 1E) and because the interconnections do not form exactly along straight lines. It is, however, much higher than the interconnection modulus determined earlier for the scaffold alone (3 MPa, Table 2), that represents that of the buckled interconnections. For high fibre volume fractions the increasing influence of the non-buckled interconnections stiffness can be observed, as the simulated stiffness closely followed the experimental results.

**Discussion**

While previous works have accessed the compressive reinforcement mechanism of hydrogel/scaffold composites related to the stretching of the fibres due to lateral expansion, in this work we are the first to consider the reinforcement mechanism due to the load transfer through the scaffold interconnections and the effect of buckling thereon. Our simulations were carried out for material properties assessed on both composite constituents independently, using experimental results, so that the predictive nature of the models as a function of fibre fraction could be validated. The important outcome of this work is that the reinforcement mechanism of the composite constructs was found to be governed by two different mechanisms. The first contribution is created by the fibres being pulled in tension by the lateral expansion of the hydrogel (Fig. 3E,F)). This mechanism dominates the reinforcement of composite constructs at lower fibre volume fractions where the number of fibre intersections is reduced, and was demonstrated by the continuum FE model. The second contribution comes from the interconnections. These interconnections are structurally more resistant than fibre walls, since they result from multiple interlocked fibres. However, the load carrying capacity of these interconnections is hardly recognized when testing scaffolds alone, due to extensive buckling of the connections. In the composite constructs, on the other hand, the surrounding hydrogel material provides lateral support and stability for the interconnections, preventing the buckling collapse observed for the scaffolds alone, and transferring the compressive load into the reinforcing fibres oriented longitudinally. The fibre interconnections behavior was observed to dominate the reinforcing mechanism for higher fibre volume fractions where they are more plentiful. It is noteworthy that buckling deformation was examined indirectly using a micro-compression device that applied and maintained strain. Each individual micro-FE model was linear, but generated for each non-linearly deformed configuration, and only
used to assess the stiffness in that deformed state. Further modelling efforts might include the observed material non-linearities, buckling effects and micro-fibre scaffold detailed geometries in a single continuum non-linear model, although such methods are computationally expensive and time-consuming.

Recent work suggested that the reinforcement mechanism was attributed to both fibre-stretching and to the high interfacial shear stresses between the hydrogel-fibres, which prevent hydrogel from flowing out the fibre scaffold. However, it was not supported by methodological calculations and further studies are required to elucidate such an assumption. Our current continuum FE model has the potential to be extended to include the rate-dependent features of the composite material and, therefore, capture such hydrogel flow. This framework can also enable to better evaluate the mechanical environment that cells will experience, which could play an important role in mediating the cell differentiation process in these novel composites. Finally, we believe that future modelling approaches should explore the reinforcement mechanism under other different loading conditions, such as shear and tension, since they play an important role in human body tissues mechanical behavior.

**Conclusion.** In the present study, we demonstrated that the reinforcement mechanism of the composite constructs is governed by two different mechanisms. The first is the pulling of the fibres in tension by the lateral expansion of the hydrogel. This mechanism dominates the reinforcement of composite constructs with lower fibre volume fraction. While the second contribution comes from load transfer through the fibre cross-section interconnections. The latter is not observed in scaffolds alone, due to buckling of the interconnections, but in the case of hydrogel composites, where the gel avoids the buckling this reinforcing mechanism dominates above a certain fibre volume fraction. Our results also provide new fundamental insights into the real structural deformation of these novel reinforced hydrogels during axial compression that can be used for assisting the design of more effective composite constructs.

**Methods**

**Materials, fabrication and characterization.** For this study, a special custom-built MEW device was developed. Air pressure regulator (FESTO, Berckheim, Germany) was used to feed the polymer melt through a 23 G spinnernet charged by a high voltage HV source (LNC 10000–5 pos, Heinzinger Electronic GmbH, Rosenheim, Germany). In order to enable an additive manufacturing process, a planar movable aluminium collector plate was mounted on top of 2 orthogonal placed axes (XSlide, Velmx, New York, USA) and controlled via an advanced 2-axis stepper motor controller (PMX-2EX-SA, ARCS Technology- Inc., USA). For a suitable temperature control of the polymer melt an electrical heating system (TR 400, HKEtect, Germany) was used. To assure stable manufacturing conditions the processing parameters were adjusted in accordance with a previous study. Accordingly, the used acceleration voltage was set to 5.5 kV at a spinning gap of 3.3 mm (E = 1.3 kV/mm), a feeding pressure of 3.0 bar and a heating temperature of 90°C was sufficient for processing GMP-PCL (PURASORB PC 12, Corbin Inc., Gorinchem, Netherlands) fibres with a desired diameter of approximately 20 µm. The collector velocity was set at 10 mm/s. Single fibres were firstly collected on a microscopic glass slide for single filament tests. Box structured meshes (5 × 5 cm²) were fabricated by alternating layer deposition orthogonally, with a filament spacing of 200, 400, 600 and 800 µm. The final height of every scaffolds was set to 1000 µm. The procedure for the preparation of GelMA-reinforced hydrogel constructs was described in detail in a previous study. MEW printed single fibres and scaffolds were imaged using a scanning electron microscopy (SEM) (Zeiss AM7515MT8A, Naarden The Netherlands) and analysed with Dino-Lite software. Images from the top of these constructs, and the original cross-sectional area for the fibre scaffolds. The lateral deformation of both composite constructs is governed by two different mechanisms. The first is the pulling of the fibres in tension by the lateral expansion of the hydrogel. This mechanism dominates the reinforcement of composite constructs with lower fibre volume fraction. While the second contribution comes from load transfer through the fibre cross-section interconnections. The latter is not observed in scaffolds alone, due to buckling of the interconnections, but in the case of hydrogel composites, where the gel avoids the buckling this reinforcing mechanism dominates above a certain fibre volume fraction. Our results also provide new fundamental insights into the real structural deformation of these novel reinforced hydrogels during axial compression that can be used for assisting the design of more effective composite constructs.

**Continuum FE model.** **Geometry and modelling assumptions.** Fibre scaffold was idealized as unidirectional lamina (Fig. 2B). The reinforcement was simulated by placing a fibre scaffold inside of a cylindrical hydrogel matrix. An embedded to model the reinforcement mechanism. In this approach element feature available in the Abaqus package was used, an embedded equation between the two meshes was created, which constrained the translation degrees of freedom of the fibre scaffold nodes (embedded part) to those of the hydrogel (host part). The elements of the hydrogel were defined by linear brick elements. The lamina were modelled by membrane elements representing the thin plate-like structure of the scaffold. At the interconnections, however, an additional truss element was added with its longitudinal axis in the global y-direction. This truss element represents the additional stiffness at the intersection due to the crossing of the fibres (Fig. 2B). Due to symmetry, only a quarter
of the composite construct geometry was considered. Similar to the experimental uniaxial compression tests described above, a vertical displacement, $d$, was prescribed on the top of the gel surface, such that the experimental strain rate of 25% min$^{-1}$ was simulated (Fig. 2B). The bottom gel surface was constrained in the compression direction and free to deform horizontally. Symmetric boundary conditions were applied to the hydrogel inner faces. Geometrically nonlinear analyses were performed. The details concerning the mesh and the geometry dimensions are given in Supplementary Table S1. FE models of pure GelMA hydrogel and of each individual scaffold were also built with the same characteristics to determine the unknown material properties for each composite constituent.

**Constitutive models.** A hyperelastic material model was chosen to characterize stress-strain behavior of the GelMA hydrogel matrix. Here, we assumed that the hydrogel matrix is homogeneous and isotropic, and therefore a simple Strain Energy Density (SED) function $U$, known as a Neo-Hookean function, that requires only two material parameters to be determined, the $C_{10}$ and $D_1$, was examined. The Neo-Hookean SED can be defined as,

$$U(T_0, f) = C_{10}(T_0 - 3) + \frac{1}{D_1}(f - 1)^2$$

where $T_0$ is the first strain invariant of the left Cauchy-Green strain tensor defined as

$$T_0 = \lambda_1^2 + \lambda_2^2 + \lambda_3^2$$

where the deviatoric stretches assume the form: $\lambda_i = j^{1/2} \lambda_i$ and $f$ is the volumetric deformation. The material parameters can then be expressed as $C_{10} = \mu_0/2$ and $D_1 = 2/K_0$, where $\mu_0$ is the initial shear modulus and $K_0$ is the bulk modulus.

Each thin lamina between the connections of the reinforcing scaffolds was assumed to behave as a linear elastic orthotropic material in plane stress. Due to the material property symmetry, the stress-strain relations related by

$$\varepsilon_{ij} = \begin{bmatrix} S_{11} & S_{12} & 0 \\ S_{12} & S_{22} & 0 \\ 0 & 0 & S_{bb} \end{bmatrix} \begin{bmatrix} \sigma_{11} \\ \sigma_{22} \\ \sigma_{bb} \end{bmatrix}$$

where the compliance elements $S_{ij}$ are related to the engineering constants as $S_{11} = 1/E_1$, $S_{12} = -\nu_{12}/E_1$, $S_{22} = 1/E_2$, $S_{bb} = 1/G_{bb}$ and $E_1$, $\nu_{12}$ and $G_{bb}$ are the elastic stiffness, Poisson’s ratio and shear modulus constants, respectively. The elements $S_{12} = 1/G_{12}$, $S_{bb} = 1/G_{bb}$ were also required to fully define the scaffold material properties, since each lamina might undergo transverse shear deformation. The fibre interconnections at the fibre-crossing points were assumed to behave like a column with stiffer transversal properties than that of the lamina. For this reason, an additional stiffness parameter $E_{int}$ was introduced to account for these interconnected fibres. These interconnections were modelled as linearly elastic. The material behaviour of the total scaffold thus was described by 6 parameters, 5 for the lamina and 1 for the interconnections.

**Assessment of the constitutive parameters.** The unknown parameters of the Neo-Hookean hydrogel model ($C_{10}$ and $D_1$), were determined by fitting the reaction force-displacement curves as measured in the experiment (see above) and those predicted from the hyperelastic continuum FE model, implementing an initial reasonable guess for the material parameters. A Matlab script was developed to optimize the material parameters using a multidimensional unconstrained nonlinear minimization method. The objective function used was defined by

$$f = \frac{1}{n} \sum_{i=1}^{n} \left( \frac{RF_{Exp}^{i} - RF_{FEM}^{i}}{RF_{Exp}^{i}} \right)^2$$

where $RF_{Exp}^{i}$ and $RF_{FEM}^{i}$ are the experimental and predicted reaction forces, respectively, and $n = 350$ is number of data points from the curve considered. The fitting procedure was repeated till the RF resulting from the computational simulations fell within the standard deviation of the experimental results.

For the lamina, the longitudinal stiffness $E_1$ was assumed to be that of the single fibre tensile stiffness as measured in the experiment divided by a factor two. The latter was done to account for the porosity introduced by the stacking nature of the fibres. The remaining 5 parameters describing the orthotropic elastic behaviour of the lamina ($E_2$, $\nu_{12}$, $G_{12}$, $G_{bb}$, $G_{bb}$) as well as the additional stiffness assumed at the interconnections ($E_{int}$), were determined by fitting the reaction force-displacement curves as measured in the experiment (see above) and those predicted from the linear elastic continuum FE model, representing only the fibre scaffold (without gel) with an 800 μm fibre spacing. The same fitting procedure as used for the hydrogel parameters was used, again starting with an initial reasonable guess for the material parameters.

**Micro FE model.** High-resolution micro-CT analysis. High-resolution images of the real composite construct architectures were obtained through different stages of compressive deformation with the use of a micro-CT scanner (µCT 80, Scanco Medical AG, Switzerland). Pure scaffolds and reinforced gels with a fibre spacing of 200...
and 800 μm were analysed at increasing compressive strain levels of 0, 15, 30 and 45%. The micro-CT device was equipped with a custom-made loading device. This loading system consists of a supporting tube driven by a bolt system and two spacers23 (Fig. 2C). When tightened, the system enabled the compression of the constructs to the required deformation level. A water-based contrast agent solution (Ioversol, Optiray 300™, Mallinckrodt Pharmaceuticals) was used in the reinforced constructs for staining the GelMA hydrogel. The acquisition parameters were set to a voltage of 70 kVp; an intensity of 114 μA and an integration time of 300 ms. After scanning, a Gauss filter was applied (sigma = 1, support = 0.8 voxel) and images were subsequently segmented. A global threshold of 24 per mile and 105–195 per mile were used for the pure scaffold and scaffold region on the reinforced hydrogel constructs.

**Micro- FE analysis.** Micro- FE models were created directly from the segmented images by using a voxel conversion procedure. Equally sized brick elements were used to generate the FE mesh of the scaffolds (≈3 M elements) and hydrogel composite phase (≈30 M elements). The micro-CT images of each deformed state, i.e. 0, 15, 30 and 45%, were used to generate the micro- FE model, and a low-friction compression test prescribing a 1% strain was performed on the deformed configuration to investigate the stiffness and the stress distribution in the deformed state. Each material phase, i.e. scaffold (E_{scaffold}, v_{scaffold}) and hydrogel (E_{gel}, v_{gel}), was modelled as a homogenous linear elastic material, described by Young’s modulus and a Poisson’s ratio. The Poisson’s ratio of the fibre scaffold was set as 0.3, equal to bulk PLC26, that of the hydrogel was set to 0.49, representing an almost incompressible material as witness by the lateral strain measurements during the compression test. The Young’s modulus of the hydrogel and of fibre were determined by fitting the reaction force as measured the experiment at 15% strain (see above) and those predicted from the micro- FE at the deformed configuration of 15% strain. Micro- FE analysis and imaging processing were performed using Scanco Finite Element software IPLFE v5.16 (Scanco Medical AG, Switzerland).

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Author Contributions
M.C., J.M., K.I designed the study. M.C., J.M., P. D.D., and J.G. developed the melt electrospinning set-up. M.C. and G.H. fabricated the scaffolds and performed the mechanical experiments. M.C., W.W., B.R. and K.I. did the FE models. K.I. supervised the study. M.C. prepared the manuscript together with all co-authors.

Additional Information
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