Serpin-loaded extracellular vesicles promote tissue repair in a mouse model of impaired wound healing

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Abstract

Chronic metabolic diseases such as diabetes are characterized by delayed wound healing and a dysregulation of the inflammatory phase of wound repair. Our study focuses on changes in the payload of extracellular vesicles (EVs) communicating between immune cells and stromal cells in the wound bed, which regulate the rate of wound closure. Adoptive transfer of EVs from genetically defined mouse models are used here to demonstrate a functional and molecular basis for differences in the pro-reparative biological activity of diabetic (db/db) vs. wildtype EVs in wound healing. We identify several members of the Serpin family of serine protease inhibitors that are absent in db/db EVs, then we overexpress Serpin A1, F2 and G1 in EVs to evaluate their effect on wound healing in db/db mice. Serpins have an important role in regulating levels of elastase, plasmin and complement factors that coordinate immune cell signaling in full thickness wounds in a diabetic model. Here, we establish a novel therapeutic approach by engineering the payload of EVs based on proteomic analysis. Serpin-loaded EVs were used to rescue the Serpin deficiency identified by proteomics and promote wound healing in db/db mice, as well as evaluated how EVs affected extracellular matrix remodeling and the resolution of tissue injury. Therefore, we propose that the identification of EV payloads that are downregulated in diabetic wounds can be systematically analyzed for their functional activity and potential as a therapeutic, based on whether their re-expression in engineered EVs restores normal kinetics of tissue repair in chronic wounds.

Keywords: Extracellular vesicles, Exosomes, Wound healing, Diabetes, Serpin, Extracellular matrix
Background
Healthy wound repair is characterized by direct and indirect intercellular interactions between cell types that mediate hemostasis, inflammation, proliferation and remodeling [1, 2]. Increasing evidence suggests that extracellular vesicles (EVs) mediate indirect signaling between cell types that is pro-reparative in wound healing [3–5]. Studies of pathways regulating EV biogenesis have demonstrated that the cellular source of EVs affects their formation, payload, and biological activity in the wound bed [6]. For example, platelet-derived EVs promote coagulation in hemostasis, while neutrophil-derived EVs regulate the expression of adhesion factors on the endothelium [7, 8]. As a wound transitions from the inflammatory phase to proliferation and re-epithelialization, macrophage-derived EVs drive macrophage polarization to an anti-inflammatory phenotype to mediate signaling between wound-edge fibroblasts and keratinocytes to promote wound closure [9]. The resolution of the inflammatory phase of wound healing involves re-epithelialization through keratinocyte migration and remodeling of granulation tissue into more permanent extracellular matrix (ECM) through expression of collagen and proteoglycans and regulation of the secretion of proteases [10–12]. In vitro studies indicate that the remodeling phase of wound healing can be stimulated by EV-mediated signaling such as in the use of mesenchymal stem cell-derived EVs that accelerate closure of chronic wounds by establishing a pro-reparative microenvironment [13, 14].

Diabetes is a chronic metabolic disease that is complicated by delayed wound healing and dysregulation of the inflammatory phase wound repair [15–19], leading to chronic wounds and substantial morbidity. To identify secreted factors in the diabetic wound bed associated with delayed cutaneous wound closure as potential therapeutic targets, we used mice lacking the Leptin receptor (Lepr−/−; db/db), which is a Type II diabetic model that is hyperglycemic and presents with a well-defined phenotype of delayed cutaneous wound closure [20–23]. We used sterile subcutaneous PVA sponge implants in mice as a source for EVs based on a recruitment of neutrophils, monocytes and macrophages similar to the inflammation phase of the wound healing [24–26]. This approach facilitated efficient EV collection that avoided cell culture artifacts including EVs that are unrelated to the wound bed, as well as artifacts associated with tissue disruption, and was compatible with species-matched genetic studies of EV biological activity. We applied this approach to genetically-defined models of impaired wound healing and report a unique signature of EVs from the wound bed of db/db mice based on their protein payload and relevance to the inflammation phase of wound healing [25, 27].

Here we have identified several members of the Serpin family of serine protease inhibitors that were down-regulated in db/db vs. wildtype (WT) EVs, which we then re-expressed, promoted wound closure. Serpins are of particular interest in wound healing because of their inhibitory effects on specific proteases that are relevant in inflammation and ECM remodeling that affects cell migration and proliferation that is a hallmark of the wound response.

Members of the Serpin superfamily regulate blood pressure, hormone transport, insulin sensitivity and the
inflammatory response [28]. The identification of Serpin deficiencies in diabetic wounds suggests the therapeutic potential of re-expression of these Serpins to promote tissue repair by modulating protease activity and inflammation responses. In combination with the emerging importance of EVs as therapeutic nanocarriers for proteins and nucleic acids in complex animal systems, our findings suggested that Serpin-loaded EVs can have a therapeutic potential in promoting closure of chronic wounds [29].

Results
Subcutaneous sponge implants as an in vivo source of EVs for allotransplantation
Implants of sterile polyvinyl alcohol (PVA) sponge elicited the recruitment of neutrophils and macrophages relevant in the inflammatory phase of wound healing, therefore, wound fluid from these implants were analyzed for cellular and EV content (Fig. 1). Immunophenotyping by flow cytometry of wound fluid cells collected over a time course of 2–14 days identified an infiltration of leukocytes such as macrophages (CD45+, CD11b+, F4/80+), inflammatory monocytes (CD45+, Ly6c+, CD11b+), dendritic cells (DCs, CD45+, CD11c+, MHCII+, CD11b+), neutrophils (CD45+, Ly6Chigh, Ly6cin), and T cells (CD4+). Neutrophils and macrophages predominated at each time point (Fig. 1a–c) followed by DCs, inflammatory monocytes and T cells. In combination with Supplementary Data showing statistical analysis (Additional file 1: Fig. S1), expression of canonical EV biogenesis genes (Additional file 1: Fig. S2 and Table. S1) and cell profiling of WT vs. db/db mice (Additional file 1: Fig. S3), these studies defined the immune cell phenotype of the implant model used as an in vivo EV source relevant to the inflammatory phase of wound healing. To characterize the EV released in the PVA sponge model, EVs were enriched by density ultracentrifugation (Fig. 1d) and analyzed by vesicle flow cytometry to demonstrate a similar EV size distribution (Fig. 1e), concentration, expression of canonical EV markers (Fig. 1f), and appearance by transmission electron microscopy (Fig. 1g) in WT and db/db EVs that was supported by vesicle flow cytometry (vFC) analysis based on MISEV2018 standards (Additional file 1: Fig. S4). Quantitative analysis of WT and db/db EVs using vFC demonstrates consistency in EV size (Additional file 1: Fig. S4 a and g) and light scatter (Additional file 1: Fig. S4 b and h). Similarly, EVs from WT and db/db mice were comparable for their staining for EV membrane phosphatidylserine using Annexin V (Fig. S4 c and i) and expression of the tetraspanins CD9, CD63 and CD81 (TS) on the EV surface (Fig. S4 d and j) with normalized expression of Annexin-V and TS expressed as histograms (Additional file 1: Fig. S4 e,f,k,l). Together, these representative plots demonstrate the analytical power of vFC for quantitative analysis of complex EV mixtures from biological fluids such as the PVA sponge and wound fluid.

Pro-reparative capacity of EVs defined by genetics of donor
To determine whether there were differences in the biological activity of WT vs. db/db EVs, we enriched EVs from PVA sponges implanted in WT or db/db mice, and adoptively transferred them into a full thickness cutaneous wound made in the dorsum of recipient db/db mice. EVs from each donor mouse genotype were administered once in either of two doses onto the wound sites of naïve db/db mice (Fig. 2a). Treatment of db/db wounds with donor EVs led to a dose-dependent acceleration of wound closure with WT EVs that contrasted with db/db EVs at the high EV dose (7.5 x 10⁵ particles/µL) (Fig. 2b). Statistically significant db/db-mediated uncoupling of the pro-reparative activity of EVs was observed at days 7–14 (Fig. 2c–g). Representative images of replicates (n = 4 at each time point for each condition) show delayed wound closure in db/db-treated EVs at the high dose (7 x 10⁵ particles/µL) (Fig. 2h) compared to treatment with WT EVs that was consistent with a delay in re-epithelialization of wounds treated with db/db EVs at day 14 (Fig. 2i, right).

Identification of changes in EV protein payloads based on mass spectrometry
Based on differences in biological activity between db/db and WT EVs in promoting wound closure, we subjected
EVs from the db/db vs. WT donors to mass spectrometry to measure changes in EV proteins that could account for differences in their biological activity. We identified 5315 proteins (Additional file 2) that were differentially expressed in db/db vs. WT EVs, with a heat map showing changes in protein expression in biological replicates (n=3 for each genotype) that were most highly down-regulated in db/db EVs (Fig. 3a, top) and proteins that

Fig. 1 (See legend on previous page.)
Fig. 2  The pro-reparative phenotype of normal wildtype EVs is delayed in EVs from db/db mice.  

a  Schematic of EV collection from sponge implants implanted in WT and db/db mice (i.e. Donor) followed by adoptive transfer to full thickness wounds into db/db mice (i.e. Recipient).  
b  Kinetics of wound closure area following treatment with EVs enriched WT vs. db/db donor mice (2-way ANOVA of WT vs db/db high dose EV treated mice, p-value < 0.0001).  
Additional statistical analysis of wound closure efficiency is shown on c Day 1, d Day 3, e Day 7, f Day 10, and g Day 14 (Means + SD, p-value: *** < 0.001, ** < 0.005, * < 0.05).  

h  Representative images of splinted wounds treated with EVs.  
i  Representative hematoxylin and eosin staining of the injury site following treatment with WT vs. db/db EVs at 14 days (Scale bars, 0.5 mm)
were up-regulated in db/db EVs compared to WT EVs (Fig. 3a, bottom). Among the proteins that were down-regulated in the db/db EVs, three protease inhibitors α-1-antitrypsin 1 (α1AT), α-2-antiplasmin (α2AP), and plasma protease C1 inhibitor (C1INH) were identified as part of the Serpin family of Serine protease inhibitors and suggested their potential relevance in wound bed hemostasis, fibrinolysis, and inflammation. Additional
Design and activity analysis of Serpin-loaded EVs in wound healing

To determine the potential of engineering EV protein payloads as therapeutics in a wound healing model, we expressed proteins of interest as in frame fusions with an amino terminal sequence that incorporated a myristoylation sequence known to lead to the post-translational delivery of proteins to EVs [30, 31]. Focusing first on the loading of a payload of interest as in frame fusions with an expression tag, we used lentivirus-mediated gene delivery to express XP-GFP in cultured HEK293 cells (Additional file 1: Fig. S5) from which EVs were enriched and subjected to a quantitative analysis to determine EV size, GFP fluorescence, tetraspanin CD81 expression, and uptake into HEK293 cells (Additional file 1: Fig. S6). These studies established that amino terminal fusions using myristoylation sequences localized proteins to EVs that were capable of delivering protein cargos to 30–50% of the cells treated with EVs as measured by GFP fluorescence. Based on these validations, we cloned each of the three Serpins identified as down-regulated in a proteomics screen to be expressed in HEK293 cells (Fig. 4a) as myristoylated fusion proteins to generate Serpin-loaded EVs (Additional file 1: Table. S2) for biochemical and activity testing. Densitometry analysis of immunoblots of EVs enriched from transduced HEK293 cells demonstrated Serpin expression in released EVs (Fig. 4b–d) compared to EVs from control parental cells. The activity of these Serpin-loaded EVs were then tested in an in vitro model of wound healing based on migration of human HaCaT keratinocyte cells [32–34]. Following removal of a dividing insert, HaCaT cells were treated once with each engineered EV type (1.20–1.7 × 10^5 particles/µL), and changes in the cell gap quantified (Fig. 4e, f). The kinetics of closure following treatment with Serpin-loaded EVs was significantly accelerated at 24 h for each of the fusion proteins expressing Serpins (SERPINA1, SERPINF2, and SERPING1) compared to the empty vector control (Fig. 4g–i).

To determine if Serpin-loaded EVs accelerated tissue repair in an in vivo model of impaired wound closure, we used a species-matched PVA sponge implant model (Fig. 5a) that combines in vivo gene transduction and EV harvest to test EV activity in vivo [6]. In this study PVA infiltrating cells were transduced in vivo with Serpin-expressing lentiviral vectors, and Serpin-loaded EVs were then harvested from the conditioned fluid of cells in the PVA implants. PVA cells were transduced with lentiviruses encoding fusions of SERPINA1, SERPINF2, SERPING1 with the same myristoylation tag used for the in vitro studies and compared with an empty vector control expressing only the tag. These EVs were enriched, counted, and the expression of the appropriate Serpin confirmed and quantified (Fig. 5b–d). To test the biological activity of the Serpin-loaded EVs, each was tested by adoptive transfer into the splinted full thickness wound model of impaired wound healing using db/db mice as the recipients. In contrast to kinetics of wound closure of PBS-treated (sham) db/db mice, wound closure was significantly accelerated by day 5 and 7 following a single dose treatment with EVs loaded with SERPINA1 and SERPING1, compared to empty vector control EVs (Fig. 5e) that was supported by representative images (Fig. 5f) and statistical analysis (Fig. 5g–k). To assess the effect of Serpin-loaded EVs on re-epithelialization we performed immunohistochemistry with an anti-cytokeratin 14 (K14) antibody and observed K14 staining within 5 days following treatment with SERPINA1 and SERPING1-loaded EVs in comparison to empty vector control (Fig. 5i). By Day 10, treatment with Serpins had increased immunostaining compared with sham and empty vector control EVs (Additional file 1: Fig. S7). Taken together these findings support the development of therapeutic EVs based on an EV loading strategy using fusion proteins and demonstrates the pro-reparative activity of SERPINA1 and SERPING1-loaded EVs in tissue repair.
Fig. 4 Testing of Serpin-loaded EV activity in vitro. 

**a** Fusions of an amino terminal myristoylation sequence with each Serpin were cloned into lentiviral vectors. 

**b-d** Validation of three Serpin-loaded EVs by immunoblotting in cultured media. Sham is PBS and Empty is the empty vector used for the myristoylation fusions. 

**e** Representative images of HaCaT cell closure kinetics. 

**f** Gap closure quantification of HaCaT cells treated with SERPINA1-EVs, SERPINF2-EVs, SERPING1-EVs, vs. empty vector, and sham (PBS). (p-value: *** < 0.001, n = 6). Statistical analysis of scratch assay on HaCaT cells by SERPIN-loaded EVs enriched from HEK293 donor cells on **g** 2 h, **h** 4 h, **i** 24 h (p-value: ** < 0.005, * < 0.05)
Fig. 5 Testing of Serpin-loaded EV activity in vivo. a In vivo strategy to transduce cells infiltrating PVA sponge implants and enrich their EVs for assessment of wound closure activity following the expression, release and enrichment of EVs loaded with SERPINA1, SERPINF2, SERPING1, and empty vector controls. b–d Validation of Serpin expression in engineered EVs by immunoblotting EVs recovered from implants, with densitometric quantification shown on the blot. e Quantification of wound closure kinetics following adoptive transfer in the db/db mouse model of impaired wound healing (2-way ANOVA, p-value < 0.0001 for SERPINA1 and SERPIN G1 vs. empty vector control, n = 6 in each arm). f Representative images of splinted wounds treated with Serpin-loaded EVs. Statistical analysis of wound closure efficiency in vivo using SERPINA1-EVs, SERPINF2-EVs, and SERPING1-EVs on g Day 3, h Day 5, i Day 7, j Day 10, and k Day 14 (p-value**** < 0.0001, *** < 0.001, ** < 0.005, * < 0.05). I Representative images of immunostaining at each time point to demonstrate expression of cytokeratin 14 at Day 5 and 10 post-injury. Statistical analysis of cytokeratin staining is shown in Fig. S7.
Discussion

The application of EVs as therapeutics to promote tissue repair highlights their translational potential; however, the molecular mechanisms of EV action remain poorly understood. Questions remain regarding what factors mediate their efficacy, the identity of relevant payloads, and how EV biology is altered in a chronic vs. normal wound bed. We have previously shown that dysregulation of EV biogenesis pathways blocks wound repair [6] by affecting protein payload and immune cell recruitment relevant to the resolution of the inflammation phase of wound repair. Here we focus on a genetically defined mouse model of Type 2 diabetes with impaired wound healing to assess EV biology in this process. We show that wildtype EVs accelerate wound closure compared to EVs from diabetic donors. Proteomic analysis of EVs isolated from diabetic mice have a deficit in the expression of a family of serine protease inhibitors, specifically Serpins A1 (anti-trypsin), Serpin F2 (anti-plasmin), and Serpin G1 (plasma protease C1 inhibitor). Given the role of Serpin A1 in inactivating elastases and Serpin F2 in regulating fibrinolysis by inactivating plasmin, and Serpin G1

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**Fig. 6** Model for Serpin-loaded EV action in accelerating a pro-resolution phenotype. (Top) In diabetic wounds, we propose that increased elastase activity increases degradation of the extracellular matrix (ECM) that can be reversed by delivery of SERPINA1-EVs to promote healthy ECM. (Middle) Decreases in plasmin inhibitor of diabetic wounds increases plasmin activity and degradation of fibrin that can be reversed by delivery of SERPINF2-EVs leading to formation of a beneficial fibrin scaffold. (Bottom) The loss of the inhibitor of the Complement C1 protease activity (C1) in diabetic mice that increases production of complement cascade products, which can be reversed by delivery of SERPING1-EVs that suppress the activation of complement cascade, activation of neutrophils, and promotes the resolution of the inflammation phase of wound repair. Created with Biorender.com
in inhibiting the complement response [35], we propose that EVs are nanocarriers of key regulatory elements responsible for coordinating hemostasis, immune cell activation and the resolution phase of wound healing. We show that re-expression of the specific Serpins in EVs that are deficient in diabetic mice accelerated wound closure in an adoptive transfer strategy, and establishes the potential for Serpins to coordinate tissue repair (Fig. 6).

Dysfunction of immune function, fibrosis, and a non-migratory epidermis are all hallmarks of the impaired wound healing responses observed in diabetic patients, including diabetic foot ulcers, for which there are limited effective therapies [1]. For example, diabetic patients fail to activate key transcriptional networks in neutrophils and macrophages that are recapitulated in diabetic mouse models. These findings suggest that the lack of coordinated signaling and immune responses contribute to impaired re-epithelialization and delayed wound closure [36]. In these examples, biochemical mediators identified as down-regulated in the diabetic wound can be re-expressed to assess their potential to rescue tissue repair in chronic wounds as we have demonstrated here with Serpin-loaded EVs.

The multiple overlapping phases of hemostasis, inflammation, proliferation, and remodeling in wound healing are both multicellular and highly coordinated, suggesting that therapeutic approaches are needed that address defects in intercellular signaling between cells that are not otherwise in direct contact. The use of the PVA sponge to generate donor EVs takes advantage of the similar immune responses with the inflammation phase of wound healing and avoids the limitations of classic cell culture methods based on cultured single cell types on plastic in the presence of serum [37]. For the evaluation of EVs in the treatment of impaired cutaneous wound healing, normal EVs have been generally collected from cultured human cells [38], with recent studies showing that delivery of specific molecules affects wound closure in the diabetic model [14].

Based on evidence that fibrinolysis and changes in the extracellular matrix (ECM) scaffolding are essential to the coordinated resolution of the inflammation phase and re-epithelialization, our findings support a role for specific protease inhibitors in these processes [39, 40]. For example, protease inhibitors such as Serpins are critical molecular switches in ECM remodeling cascades that affect the recruitment of immune cells and re-epithelialization through a combination of direct contact and indirect intercellular signaling. Based on the pro-reparative potential of EVs in the diabetic wound [22, 41], our analysis of isolated wildtype and diabetic EVs has identified distinct protein payloads and biological activities in mediating wound repair. The impaired expression of protease inhibitors in diabetic wound EVs underscores the importance of specific proteases that mediate remodeling of the ECM, drive the recruitment and activation of immune cells in wound closure, and are indicative of a more general dysfunction of proteases in diabetic wounds.

For example, Serpin A1 encodes the alpha1-proteinase inhibitor (α1PI), which acts upon trypsin as well as neutrophil elastases [42]. Diabetic wounds have increased elastase associated with infection and worsening of ulcers [43], consistent with our observation of decreased levels of the Serpin A1/α1PI elastase inhibitor in diabetic wound EVs. While the mechanisms of EV-mediated Serpin A1 have yet to be elucidated, Serpin A1/α1PI also has non-enzymatic activity in its ability to bind to the cell surface and promote migration [29, 42]. Surface binding of EVs, especially at the leading edge where membrane-bound EVs loaded with ECM-remodeling protease/protease inhibitors, can enhance cell migration by modifying intracellular actin re-organization that promotes directional cell adhesion [44]. Other examples of the pathogenesis of reduced Serpin A1/α1PI levels include increased neutrophil elastase in the bloodstream leading to acute inflammation, degradation of lung elasticity, and liver cirrhosis [42].

The decreased levels of Serpin F2/antiplasmin observed in EVs in the diabetic wound support the role for factors regulating coagulation and fibrinolysis in wound healing [45]. In wound healing, mice lacking plasminogen, the zymogen form of plasmin, tissue plasminogen activator or urokinase plasminogen activator all have impaired wound healing responses [46, 47]. While free Serpin F2/antiplasmin inhibits plasmin formation, the fibrin-bound form regulates clot lysis [45]. Studies of mice lacking Serpin F2/antiplasmin show accelerated angiogenesis and wound closure [48] further supporting a role for the fibrinolytic cascade in regulating wound closure kinetics, although the timing and localization of specific targets remain poorly understood. Therefore, wound healing disorders may respond to increases in protease inhibitors such as Serpin F2/antiplasmin that accelerate fibrinolysis and promote conversion of a wound microenvironment from pro-inflammatory to pro-resolution and increased wound closure [49].

Serpin G1/C1-inhibitor is an acute-phase protein that increases in the circulation in response to injury, and functions to inhibit the complement system. Deficiency in Serpin G1/C1-inhibitor also permits kallikrein activation, and the production of the vasoactive peptide bradykinin [50]. In the wound bed, administration of a Serpin G1/C1-inhibitor reduces local inflammation and capillary
leakage, although the acceleration of wound closure may depend on the duration of Serpin G1/C1-inhibitor administration [51, 52]. With Serpins often classified as acute phase proteins that regulate inflammation, expressing specific Serpins in EVs may promote wound closure by delivering enzyme inhibitors in EVs that have an EV-dependent tropism for specific microenvironments of the wound bed. For example, elastase levels in diabetic ulcer tissue were significantly higher in wounds with infections and presented with a delayed wound healing profile [53]. Moreover, EVs delivering enzymes that regulate the remodeling of ECM can localize protease inhibitors at the interface of plasma membrane and release protein payloads at membrane domains regulating the leading edge of migrating cells [54].

The rationale for the delivery of EVs loaded with specific protein payloads is based on the identification of specific Serpins that are down-regulated in the diabetic EVs, which can then be tested for their capacity to restore wound closure kinetics of a wild type full thickness wound. Our strategy uses lentiviral constructs to express a target protein as a fusion with a membrane domain that traffics proteins to EVs and anchors them to the membrane [30, 55]. Membrane domains that mediate the trafficking of protein payloads into EVs based on a myristoylation domain have similarities with viral budding that can be exploited for delivery of custom EV protein payloads [56–58].

EV-based therapies have emerged as a significant area of interest in the treatment of ischemia, infection, impaired wound healing, and cancer; however, none are FDA-approved to date. The over-arching concept behind the development of EV-based therapeutics is their potential as stable delivery vehicles of payloads that regulate intercellular signaling, especially when compared to small molecules in solution or cell therapy [59]. EVs are complex in terms of the range of their protein and nucleic acid payloads, and heterogenous in terms of the different populations of EVs present in a multi-cellular microenvironment where a given cell type may release different EVs depending on its metabolism and activation state [6]. As in our previous EV proteomic studies [6, 60], we use proteomics to identify proteins that are differentially expressed in EVs which in this study we show can be rescued using a re-expression system. The use of a species and strain-matched donors for the collection EVs for the analysis of the effect of the diabetic host on their EV payload is essential for the determination of their ability to promote wound closure following adoptive transfer into a full thickness chronic wound.

Conclusions

The discovery of a deficiency of Serpin expression in the EVs of diabetic mice led to the hypothesis that over-expression of such Serpins in engineered EVs could be used to rescue impaired wound healing. The combination of target discovery leading to the development of Serpin-loaded EVs established the biological activity of engineered Serpins with applications that may well extend beyond the molecular targets and injury models tested here.

Methods

Mice, PVA sponge implants and wound healing assays

All animal experiment were conducted in accordance with the protocols approved by the Institutional Animal Care and Use Committee of the University of California, San Diego. Male 10–16-week-old C57BL/6J mice (JAX #0664) and Leprdb/db mice (JAX #0697) were maintained on a 12 h light/dark cycle. Subcutaneous implants of sterile polyvinyl alcohol (PVA) sponges (PVA unlimited, Warsaw, IN, USA) inserted (n = 3 per site) in dorsum of each animal and the surgical site closed with nylon monofilament suture (# MV-663-V-19 mm, Oasis, IL, USA) [25, 61]. Animals recovered in the presence of sufficient food and water supply. Mice bearing PVA sponges were incubated as indicated for up to 14 days, the sponges removed under anesthesia, transferred into 500 µl of PBS in a microtube, and the sponges briefly compressed with a forceps 3–4 times to release cells and EVs from the sponge. The sponges were then removed, and cells separated from the PVA fluid by centrifugation at 300 × g for 5 min for analysis by flow cytometry and quantitative PCR, while EVs were enriched from the supernatant for in vitro testing as described below and tested in adoptive transfer assays into full thickness wounds in naïve db/db mice. For these assessments of EV activity upon the kinetics of wound healing assay in the db/db model, hair was removed, a full thickness 4 mm punch made (#P450, Acuderm inc., FL, USA), the site splinted with silicone ring (Thickness: 0.5 mm, outside diameter: 12 mm, inside diameter: 6 mm) (#33,350,174, MCS, Mableton, GA, USA) and the ring immobilized with nylon suture as previously described [18, 62] were. EVs were added to the wound site in 10–50 µL, covered with Tegaderm (#1622w, 3M, Maplewood, MN, USA), and the wound site imaged daily with a digital camera (Galaxy 10e, 1200 pixels, AF, F1.5/F2.4 super speed dual pixel, Samsung, Seoul, Korea) and analyzed by Image J (1.53e version, National Institutes of Health,
Bethesda, USA). Hematoxylin and eosin-stained tissue sections of skin were prepared from formaldehyde fixed paraffin embedded, and cryosections prepared in Tissue-Tek® OCT compound (Cat#4583, Sakura® Fine-tek, Torrance, CA, USA), stained with Cytokeratin 14 antibodies (Cat#10,143-1-AP, Proteintech, Rosemont, IL, USA) and imaged with a laser scanning confocal microscope (ECLIPSE Ti2, Nikon Instruments Inc. Melville, NY, USA). These EV assays were used for the assessment of WT vs db/db EV activity as well as for the analysis of EV engineered to express specific Serpins as described below. In both studies, EVs were prepared from mice bearing PVA sponge implants, enriched, quantified and then adoptively transferred to full thickness splinted wounds as described above.

Flow cytometry
For the analysis of cells recruited to the PVA sponge model used for the harvest of EVs, cells were subjected to flow cytometry using Fc block (Cat#130-092-575, Miltenyi Biotec, San Diego, CA, USA), followed by staining with antibodies specific for the following immune cell markers from Miltenyi Biotec (CD11b, #130-109-287; CD11c, #130-110-840; CD45, #130-110-803; CD44, #130-119-127; F4/80, #130-102-422; Gr1, #130-102-233; Ly6G, #130-107-912, Ly6C, #130-123-796, MHCII, #130-119-122; CD4, #130-118-696, and CD3, #130-117-788). Propidium iodide (#130-093-233, Miltenyi Biotec, San Diego, CA, USA) and analyzed using FlowJo software (Version 10.7.1, Becton, Dickinson and Company, Franklin Lakes, NJ, USA).

Isolation of EVs
EV isolation from PVA sponge implants was based on density gradient ultracentrifugation as previously described [4, 63, 64], with an initial spin of 10,000×g for 30 min at 4 °C to separate EVs from the PVA fluid. Opti prep gradient (#D1556, Sigma Aldrich, CA, USA), was prepared as 8% (1.068 g/ml), 10% (1.078 g/ml), 14% (1.098 g/ml), 20% (1.127 g/ml), 26% (1.156 g/ml), and 30% (1.175 g/ml) solutions layers overlaid with supernatant in polycarbonate ultracentrifuge tube (#343,778, Beckman coulter, CA, USA) (Rotor #TS55, k factor: 50 k, Beckman coulter), and fractionated at 259,000×g (Accel:4/Decel:9) for 2 h in a Beckman Optima Max-XP Ultracentrifuge. After centrifugation, 10×100 µl fractions were collected, protein concentration determined by BCA assay (#23,227, Thermo Fisher Scientific, Waltham, MA, USA). For assays of protein expression, EVs were solubilized in RIPA lysis buffer (#89,901, Thermo Fisher Scientific), while for quantification of EV size, concentration, mass spectrometry, vFC or biological activity, EVs from control and experimental groups were normalized based on concentration as indicated.

EVs isolated from cultured media for in vitro assays was performed using Exoquick kit (#EQUILTRA-20A-1, SBI, CA, USA) and following manufacturer’s recommendations. Briefly, cell culture medium was centrifuged at 3000×g for 15 min to remove cell debris, supernatant transferred to a new tube and incubated overnight at 4 °C with Exoquick. The Exoquick/media mixture was centrifuged at 3000×g for 10 min, the supernatant aspirated, and the pellet resuspended in PBS for subsequent concentration, sizing, immunoblotting and biological activity studies.

Quantification of EVs and concentration and size distribution by vesicle flow cytometry
EV samples diluted by PBS, and stained with a fluoro-genic membrane stain (vFRed, Cellarcus Biosciences), a cytoplasmic stain (CFSE, Cellarcus) and EV surface markers in a total volume of 50 µl in a 96 well v bottom plate for 1 h at ambient temperature, according to manufacturer’s instructions. The optimal concentrations of antibody and other reagents was determined by the manufacturer via titration and provided at 10× the final staining concentration. Stained samples were diluted 1000-fold in vesicle staining buffer and analyzed on the flow cytometer. The dilutions series protocol determines the EV concentration, assay dynamic range, and the optimal dilution for subsequent cargo analysis.

Transmission electron microscopy
For the imaging of EVs by transmission electron microscopy (TEM) on grids, the PELCO easiGlow system (91000S, Ted Pella, Inc) was using for hydrophilization onto grids (Cat# 01,754-F, Formvar, 200 mesh, copper, Ted Pella, Inc., Redding, CA, USA). Grids were washed onto grids (Cat# 01,754-F, Formvar, 200 mesh, copper, Ted Pella, Inc., Redding, CA, USA) and following manufacturer’s recom-
da was used to exclude dead cells. Isotype antibodies were used for all fluorescence studies. (VioBlue/PacBlue, #130-113-454; VioGreen/BV510, #130-113-456; FITC, #130-113-449; PE, #130-113-450; PE-Vio770, #130-113-452; APC, #130-113-446; and APC-Vio770/Fire750, #130-113-447, Miltenyi Biotec, CA, USA). All flow cytometry was performed on a MACSQuant 10 instrument (Miltenyi Biotec, San Diego, CA, USA) and analyzed using FlowJo software (Version 10.7.1, Becton, Dickinson and Company, Franklin Lakes, NJ, USA).

For the imaging of EVs by transmission electron microscopy (TEM) on grids, the PELCO easiGlow system (91000S, Ted Pella, Inc) was using for hydrophilization onto grids (Cat# 01,754-F, Formvar, 200 mesh, copper, Ted Pella, Inc., Redding, CA, USA). Grids were washed and stained with uranyl acetate, and imaged with a Jeol 1400 plus TEM at 80 keV (Jeol USA, Peabody, MA, USA).

Sample preparation and LC-Mass Spectrometry
EVs samples from PVA implants were isolated by density ultracentrifugation as described above and analyzed in the Biomolecular and Proteomics Mass Spectrometry Facility at UCSD. For each sample, guanidine-HCl

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Sample preparation and LC-Mass Spectrometry
EVs samples from PVA implants were isolated by density ultracentrifugation as described above and analyzed in the Biomolecular and Proteomics Mass Spectrometry Facility at UCSD. For each sample, guanidine-HCl
was added to each sample to final concentration of 6 M, boiled for 10 min and cooled at room temperature for 5 min, with this cycle repeated three times. Following methanol precipitation and removal of the supernatant, the pellet was suspended in 8 M Urea in 100 mM (Tris pH 8.0). Samples were brought to a final concentration of 10 mM TCEP (2-carboxyethyl phosphine) and 40 mM Chloro-acetamide solution. Three volumes of 50 mM Tris pH 8.0 were added to the sample to reduce the final urea concentration to 2 M. Trypsin was added (1:50 ratio), incubated at 37 °C for 12 h, samples acidified using TFA (0.5% TFA final concentration) and desalted using C18-StageTips (#87,782, Thermo Fisher) as described by the manufacturer protocol. The peptide concentration of sample was measured using BCA after resuspension in TMT buffer. For high pH fractionation, the Pierce™ High pH Reversed Phase Peptide Fractionation Kit (#84,868, Thermo Fisher) to generate 8 unique peptide fractions that were analyzed by ultra-high-pressure liquid chromatography (UPLC, Thermo Dionex Ulti-Mate™ 3000 RSLC nano System) (#ULTIM3000RSLC-NANO, Thermo Fisher) coupled with tandem mass spectroscopy (LC-MS/MS) using nano spray ionization. The nano-spray ionization experiments were performed using an Orbitrap fusion Lumos hybrid mass spectrometer (Model#IQLAEEGAPFADBMBHQ, Thermo Fisher) interfaced with nanoscale reversed-phase UPLC using a 25 cm, 75-micron ID glass capillary packed with 1.7-µm C18 (130) BEHTM beads (Waters corporation). Peptides were eluted from the C18 column into the mass spectrometer using a linear gradient (5–80%) of ACN (Acetonitrile) at a flow rate of 375 µL/min for 120 min. The buffers used to create the ACN gradient were: Buffer A (98% H2O, 2% ACN, 0.1% formic acid) and Buffer B (100% ACN, 0.1% formic acid). Mass spectrometer parameters are as follows; an MS1 survey scan time of 50 ms) was followed by data dependent scans (top 1–2 ions, and 5 s exclusion time, while selecting ions with minimal intensities of 50,000 at which the collision event was carried out in the high energy collision cell (HCD Collision Energy of 38%) and the first quadrupole isolation window was set at 0.8 (m/z). The fragment masses were analyzed in the orbitrap detector (mass range (m/z) by automatic scan with first scan at m/z = 100. The resolution was set at 30,000 resolutions. The AGC Target set to 30,000, and maximum injection time was 54 m-sec. Protein identification and quantification was carried out using Peaks Studio 8.5 (Bioinformatics solutions Inc., Canada).

Western blot
All EVs subjected to immunoblotting were quantified by BCA assay kit (#23,225, Thermo Fisher), samples prepared in NuPAGE™ LDS Sample Buffer (#NP0008, Thermo Fisher), separated using the 12% Bis-Tris Mini Gel (#NP0342BOX, Thermo Fisher), transferred to PVDF membrane (#LC2005, 0.45 µm, 8.3 × 7.3 cm, Thermo Fisher), and blocked with 3% Nonfat Dry Milk Cell (NFDM) (Cat# 9999, CST, MA, USA) in 1X Tris-buffered saline (#9997, CST, MA, USA) with 0.05% Tween 20. Primary antibodies used were CD81 (#10,037, CST), CD63 (#PA5-92,370, Invitrogen, USA), CD9 (#PA-5–85,955, Invitrogen), Alix (#92,880, CST), SERPINA1 (#TA500374s, Origene, USA), SERPINF2 (#PA5-81,014, Thermo Fisher), and SERPING1 (#PA5-81,015, Thermo Fisher) at a 1/1000 dilution. Anti-rabbit IgG, HRP-linked (#7074, CST) or anti-mouse IgG, HRP-linked antibodies at 1/1000 dilution (Cat# 7076, CST, USA) were used as secondary antibodies, and blot incubated with Pierce™ ECL western blotting substrate reagent (#32,209, Thermo Fisher), blots imaged with a Xenogen IVIS-Lumina (Caliper Life Sciences Inc., Hopkinton, MA, USA) and the band intensities quantified using Living Image software (Ver.4.3.1, Caliper Life Sciences).

Cloning and Lentivirus production
Lenti-X 293 T cells (#632,180, TakaraBio) were used for the production of lentivirus based on Lenti-XPack vectors (System Biosciences, Palo Alto, CA) that contained the EV signal peptides as an N-terminal fusion with a multiple cloning site (pLenti-XPack-MCS (#XPA-K710PA-1) or as fusion with GFP (pLenti-XPack-GFP, #XPAK510PA-1). Primer design tools from TAKARA (https://www.takarabio.com/learning-centers/cloning/primer-design-and-other-tools) were used to amplify SERPIN genes from cDNAs (Origene) encoding human SERPINA1 (#RC202082), SERPINF2 (#RC228342) or SERPING1 (#RC203767) flanked by Xho I and NotI restriction enzyme sites for cloning into pLenti-XPack-MCS vector. The following primers were used for SERPINA1-F (5’- GCA AAG ATG CCT CGA GGA TGC CGT CTT CTG TCT CGT G -3’) and SERPINA1-R (5’- AGA ATT CTC GCG GCC GCT TAT TTT TGG GTG GGA TTC ACC AC -3’); SERPINF2-F (5’- GCA AAG ATG CCT CGA GGA TGG CCG CGC TGC TCT GGG G -3’) and SERPINF2-R (5’- AGA ATT CTC GCG GCC GCT CAC TTG GGG CTG CCA AAC TGG -3’) and SERPING1-F (5’- GCA AAG ATG CCT CGA GGA
Serpin-loaded EV activity cell migration assay

HEK293T (CRL-1573, ATCC, Bethesda, MD) cells were transduced with lentivirus (10,000 to 15,000 particles), incubated for 48 h in serum complete media, and then washed with PBS and the media replaced with a serum-free medium for an additional 24 h. From this serum-free medium, EVs were concentrated, quantified, and immunoblotted as described above prior to testing in a migration assay using HaCaT cells cultured on 2-well dishes (#81,176, Ibidi, Gräfelfing, Germany). After 24 h seeding of cells, an insert was removed, the cell culture media replaced with EV-containing media as described, cells imaged over 24 h using a CCD camera (Retiga R6, Tel-edyne photometrics, Tucson, AZ, USA) on an Olympus IX70 microscope to measure changes in cell migration. All images analyzed using OCULAR v1.0.3.110 software and Image J.

Statistical analysis

All statistical analyses were performed with Prism 6.0 (Graphpad Software, La Jolla, CA, USA). Descriptive results of continuous variables were expressed as the mean ± standard deviation (SD) for normally distributed variables. Differences between different groups were compared by ANOVA for analysis of two or more groups in the kinetic studies, and Student’s t-test for pairwise comparisons with p-values indicated as ****<0.0001, ***<0.001, **<0.005, *<0.05 considered to be statistically significant. All statistical analyses and representative images are presented as observed in at least 3 independent experiments.

Abbreviations

EV: Extracellular vesicles; Serpin: serine protease inhibitor; α1AT: Alpha-1-proteinase inhibitor; α2AP: α-2-Antiplasmin; C1INH: Plasma protease C1 inhibitor; ECM: Extracellular matrix; PVA: Polyvinyl alcohol; WT: Wild type; GFP: Green fluorescent protein.

Supplementary Information

The online version contains supplementary material available at https://doi.org/10.1186/s12951-022-01656-7.

Additional file 1: Figure S1. Statistical analysis of CD marker expression in PVA infiltrates at various time points. In support of the piechart analyses in Fig. 1, immune cells infiltrating PVA sponges were quantified at each time point focusing on: a macrophages, b inflammatory monocytes, c neutrophils, d dendritic cells, and e T cells (p-value: ***<0.001, **<0.005, *<0.05). Figure S2. Evaluation of EV biogenesis related gene expression in the PVA cells by qRT-PCR depending on the 2, 7, and 14 days. Measurements of changes in gene expression normalized to GAPDH in cells infiltrating PVA sponges focusing on the following canonical biogenesis genes: a Rab3a, b Rab35, c Rab27a, d Rab27b, e Rab11a, f VPS4a, g TSG101, and h Rab35 (p-value: **<0.001). Figure S3. Analysis of baseline cell infiltrate in PVA sponges of WT vs. db/db mice, from which EVs were harvested. Flow cytometry analysis of immune cells recruited to the PVA sponge at 14 days post-implantation focusing on: a monocytes based on CD11bLy6Chigh cells as a subset of CD45^- cells, b neutrophils based on Ly6G^Ly6Chyat cells as a subset of CD45^ cells, c macrophages based on CD11b^CD45^- cells as a subset of CD45^- cells, d dendritic cells based on CD11b^CD11c^- cells, e T cells based on CD4^ cells as a subset of CD3^ cells, f CD8^ T cells as a subset of CD3^ cells, g regulatory T cells based on CD4^CD25^ cells as a subset of CD3^ cells. (p-value: <0.05). Figure S4. Validation of EVs derived from WT and db/db mice by vFRED analysis: a size distribution of WT EVs, b Plot diameter data of WT EVs. c Expression of Annexin V-PE on WT EVs. d Expression of tetraspanins CD9, CD63 and CD81 (TS-Pe) on WT EVs. e Histogram of Annexin V-PE expression on WT EVs normalized to buffer only (grey filled in). f Histogram of TS-PE on WT EVs normalized to buffer only (grey filled in). g Size distribution of db/db EVs. h Plot diameter data of db/db EVs. i Expression of Annexin V-PE on db/db EVs. j Expression of CD81. k Histogram of Annexin V-PE expression on db/db EVs normalized to buffer only (grey filled in). l Histogram of TS-PE on db/db EVs normalized to buffer only (grey filled in). Figure S5. Validation of lentivirus titer testing using HEK293 cells. a Representative comparison of lentivirus yields based on titer testing of lentiviral p24 protein using GoStix analysis per manufacturers recommendations. Figure S6. A representative example of the analysis of EVs engineered to express specific proteins. a EVs collected from the conditioned media of parental cells as a negative control (Left, naive HEK293 donor cells) and enriched by density ultracentrifugation were subjected to vFRED staining to determine EV diameter as described in the Materials and Methods. b GFP-loaded EVs (XP-GFP) in absence (Left) or presence (Right) of anti-CD81-PE tetraspanin were analyzed for b GFP fluorescence and c expression of CD81. d and e An overview and quantification of GFP-EV internalization into HEK293 cells (filled in) compared to buffer control (open). Figure S7. Quantification of K14 immunohistochemistry. The fluorescent intensity of anti-K14 stained tissue sections from Figure S1 were quantified using Image J. A minimum of 3 fields were analyzed for each of the EV treated samples (p-value: *<0.05). Table S1. Detail information of primer for extracellular vesicle biogenesis related genes. Table S2. Primer sequences for cloning of XP tag in-frame with SERPIN1A1, SERPIN1F2, and SERPING1.

Additional File 2: Proteomic data from the Mass Spectrometry analysis of proteins detected in EVs from wild-type and diabetic db/db mice.
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Author contributions

D.J.P. and B.P.E designed this study of extracellular vesicles. D.J.P, E.D, and J.N analyzed extracellular vesicle in PVA sponges. R.D. and M.D. analyzed biological statistical data. D.J.P, B.P.E, and J.N wrote the first draft of manuscript, and all authors have reviewed the manuscript. All authors read and approved the final manuscript.

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Availability of data and materials

Data supporting the primary findings are included in the main figures, the Supplementary Data, with additional data regarding EV characterization available upon request.

Declarations

Ethics approval and consent to participate

Not applicable as there were no human studies. Mouse studies were approved by the UCSD IACUC as described in the Materials and Methods.

Consent for publication

All authors agree.

Competing interests

The authors declare that they have no competing interests.

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References

1. Eming SA, Martin P, Tomic-Canic M. Wound repair and regeneration: mechanisms, signaling, and translation. Sci Transl Med. 2014;6:265ra266.

2. Wilkinson HH, Hardman MJ. Wound healing: cellular mechanisms and pathological outcomes. Open Biol. 2020;10:200223.

3. Gutierrez-Vazquez C, Villarroya-Beltri C, Mittelbrunn M, Sanchez-Madrid F. Transfer of extracellular vesicles during immune cell-cell interactions. Immunol Rev. 2013;251:125–42.

4. Hettich BF, Ben-Yehuda Greenwald M, Werner S, Leroux JC. Exosomes for vascular inflammation and tissue repair. Front Pharmacol. 2019;10:1479.

5. Zhou X, Brown BA, Siegel AP, El Masry MS, Zeng X, Song W, Das A, Khan-delval P, Clark A, Singh K, et al. Exosome-mediated crosstalk between keratinocytes and macrophages in cutaneous wound healing. ACS Nano. 2020;14:12732–48.

6. Lipson KE, Wong C, Teng Y, Spong S. CTGF is a central mediator of tissue remodeling and fibrosis and its inhibition can reverse the process of fibrosis. Fibrogenesis Tissue Repair. 2012;5:524.

7. Wang PH, Huang BS, Horig HC, Yeh CC, Chen YJ. Wound healing. J Chin Med Assoc. 2018;81:94–101.

8. Wei F, Wang A, Wang Q, Han W, Rong R, Wang L, Liu S, Zhang Y, Dong C, Li Y. Plasma endothelial cells-derived extracellular vesicles promote wound healing in diabetes through YAP and the PI3K/Akt/mTOR pathway. Aging (Albany NY). 2020;12:12002–18.

9. Wang P, Huang BS, Horig HC, Yeh CC, Chen YJ. Wound healing. J Chin Med Assoc. 2018;81:94–101.

10. Wei F, Wang A, Wang Q, Han W, Rong R, Wang L, Liu S, Zhang Y, Dong C, Li Y. Plasma endothelial cells-derived extracellular vesicles promote wound healing in diabetes through YAP and the PI3K/Akt/mTOR pathway. Aging (Albany NY). 2020;12:12002–18.

11. Wang PH, Huang BS, Horig HC, Yeh CC, Chen YJ. Wound healing. J Chin Med Assoc. 2018;81:94–101.

12. Wei F, Wang A, Wang Q, Han W, Rong R, Wang L, Liu S, Zhang Y, Dong C, Li Y. Plasma endothelial cells-derived extracellular vesicles promote wound healing in diabetes through YAP and the PI3K/Akt/mTOR pathway. Aging (Albany NY). 2020;12:12002–18.

13. Park DJ, Park JE, Lee SH, Eliceiri BP, Choi JS, Seo YJ. Protective effect of MSC-derived exosomes against cisplatin-induced apoptosis via heat shock protein 70 in auditory explant model. Nanomedicine. 2021;38:102447.

14. Wang C, Wang M, Xu T, Zhang X, Lin C, Gao W, Xu H, Lei B, Mao C. Engineering bioactive self-healing antibacterial exosomes hydrogel for promoting chronic diabetic wound healing and complete skin regeneration. Theranostics. 2019;9:765–76.

15. Dlugonska H, Gatkowska J. Exosomes in the context of toxoplasma gondii - host communication. Ann Parasitol. 2020;16:169–74.

16. Koh TJ, DiPietro LA. Inflammation and wound healing: the role of the macrophage. Expert Rev Mol Med. 2011;13:e23.

17. Leoni G, Neumann PA, Sumagin R, Denning TL, Nusrat A. Wound repair: role of immune-epithelial interactions. Mucosal Immunol. 2015;8:599–68.

18. Jr M, Churin SS, Bleichman KM, Greives MR, Arabii S, Galiano RD, Gurtner GC. db/db mice exhibit severe wound-healing impairments compared with other Murine diabetic strains in a silicone-splinted excisional wound model. Wound Repair Regen. 2007;15:665–70.

19. Pang J, Mainschein-Cline M, Koh TJ. Enhanced Proliferation of Ly6C(+) Monocytes/Macrophages Contributes to Chronic Inflammation in Skin Wounds of Diabetic Mice. J Immunol. 2021;206:621–30.

20. Ackerman JE, Geary MB, Orner CA, Bawanya F, Loisel MA. Obesity/Type II diabetes alters macrophage polarization resulting in a fibrinoid tendon healing response. PLoS ONE. 2017;12:e0181127.

21. Leszcynska A, Kulkarni M, Lubimov AV, Saghizadeh M. Exosomes from normal and diabetic human corneal keratocytes differentially regulate migration, proliferation and marker expression of limbal epithelial cells. Sci Rep. 2018;8:15173.

22. Li M, Wang T, Tian H, Wei G, Zhao L, Shi Y. Macrophage-derived exosomes accelerate wound healing through their anti-inflammation effects in a diabetic rat model. Artif Cells Nanomed Biotechnol. 2019;47:3793–803.

23. Patel S, Srivastava S, Singh MR, Singh D. Mechanistic insight into diabetic wounds: Pathogenesis, molecular targets and treatment: strategies to pace wound healing. Biomed Pharmacother. 2019;112:108615.

24. Baird A, Deng C, Eliceiri MH, Hagh F, Dang X, Coimbra R, Costantini TW, Torbett BE, Eliceiri BP. Mice grafted with human hematopoietic stem cells support a human myeloid cell inflammatory response in vivo. Science. 2020;369:12002396.

25. Than UT, Guanzon D, Levesley D, Parker T. Association of extracellular membrane vesicles with cutaneous wound healing. Int J Mol Sci. 2017. https://doi.org/10.3390/ijms18050956.

26. Qin S, Doroshchen RA, Masini I, Lavoie-Gaigne O, Stahl PD, Costantini TW, Baird A, Eliceiri BP. TBC1D3 regulates the payload and biological activity of extracellular vesicles that mediate tissue repair. FASEB J. 2019;33:6129–39.

27. Lopez E, Srivastava AK, Burchfield J, Wang YW, Cardenas JC, Togarrati PP, Miyazawa B, Gonzalez E, Holcomb JB, Pati S, Wade CC. Platelet-derived extracellular vesicles promote hemostasis and prevent the development of hemorrhagic shock. Sci Rep. 2019;9:17676.
31. Yang JM, Gould SJ. The cis-acting signals that target proteins to exosomes and microvesicles. Biochem Soc Trans. 2013;41:277–82.
32. Huang TH, Kuo HC, Yang YL, Wang FS. MicroRNA-29a is a key regulator that regulates BRD4 and mitigates liver fibrosis in mice by inhibiting hepatic stellate cell activation. Int J Med Sci. 2019;16:213–20.
33. Liu F, Hu S, Yang H, Li Z, Huang K, Su T, Wang S, Cheng K. Hypauronic Acid Hydrogel Integrated with mesenchymal stem cell-secretome to treat endometrial injury in a rat model of Asherman’s syndrome. Adv Healthc Mater. 2019;8:e1900111.
34. Pitzurra L, Jansen ID, de Vries TJ, Hoogkamp MA, Loos BG. Effects of L-PRF and A-PRF on periodontal fibroblasts in vitro wound healing experiments. J Periodontal Res. 2020;55:287–95.
35. Kawano N, Nagai N, Okada K, Okumoto K, Ueshima S. Matsuos. Role of plasminogen in macrophage accumulation during liver repair. Thromb Res. 2010;125:e214-221.
36. Sawaya AP, Stone RC, Brooks SR, Pastar J, Jozic I, Hasneen K, O’Neill K, Mehdizadeh S, Head CR, Stibro N, et al. Derenatured immune cell recruitment orchestrated by FXM1: impairs human diabetic wound healing. Nat Commun. 2020;11:4678.
37. Kasewicz LN, Whitehead KA. Recent advances in biomaterials for the treatment of diabetic foot ulcers. Biomater Sci. 2017;5:1962–75.
38. Narauskaite D, Vymantaitė G, Rusteika J, Sampath R, Rudyte A, Stasiute G. Aparicio Calvente MJ, Jekabsons A. Extracellular vesicles in skin wound healing. Pharmaceuticals (Basel). 2021. https://doi.org/10.3390/ ph14080811.
39. Major MR, Wong VW, Nelson ER, Longaker MT, Gurtner GC. The foreign body response: at the interface of surgery and bioengineering. Plast Reconstr Surg. 2015;135:1489–98.
40. Pang J, Maenschm-Cline M, Kish TJ. Reduced apoptosis of monocytes and macrophages is associated with their persistence in wounds of diabetic mice. Cytokine. 2021;142:155516.
41. Petkovic M, Sorensen AE, Leal EC, Carvalho E, Dalgaard LT. Mechanistic actions of microRNAs in diabetic wound healing. Cells. 2020. https://doi.org/10.3390/cells9102228.
42. Guttmann O, Baranovskiy BM, Schuster R, Kaner Z, Freixo-Lima GS, Bahar N, Kalay M, Mazrihi M, Brami I, Ochayon DE, Lewis EC. Acute-phase protein alpha1-anti-trypsin: diverting injurious innate and adaptive immune responses from non-authentic threats. Clin Exp Immunol. 2015;179:161–72.
43. Fadin GP, Menegazzo L, Rigato M, Scattolin V, Ponzina N, Bruttoccao A, Cicciiolet S, Mammano F, Cibotarou CD, Brocco E, et al. NETosis delays diabetic wound healing in mice and humans. Diabetes. 2016;65:1061–71.
44. Lu Y, Kaddour H, Kopcho S, Panzieri TD, Shouman N, Kim EY, Martinson J, McKay H, Martinez-Maza O, Margolick JB, et al. Human immunodeficiency virus (HIV) infection and use of illicit substances promote secretion of semen exosomes that enhance monocyte adhesion and induce actin reorganization and chemotactic migration. Cells. 2019. https://doi.org/10.3390/cells8091027.
45. Coughlin PB. Antiplasmin: the forgotten serpin? FEBS J. 2005;272:4852–7.
46. Romer J, Bugge TH, Pyke C, Lund LR, flick MJ, Degen JL, Dano K. Impaired wound healing in mice with a disrupted plasminogen gene. Nat Med. 1996;2:287–92.
47. Bugge TH, Flick MJ, Danton MJ, Daugherty CC, Romer J, Dano K, Carmeliet P, Collen D, Degen JL. Urkonase-type plasminogen activator is effective in fibrin clearance in the absence of its receptor or tissue-type plasmino- gen activator. Proc Natl Acad Sci U S A. 1996;93:9599–904.
48. Kanno Y, Hirade K, Ishisaka A, Nakajima K, Suga H, Into T, Matsuha K, Okada K, Matsuos O, Matsuho L. Lack of alpha2-antiplasmin improves cutaneous wound healing via over-released vascular endothelial growth factor-induced angiogenesis in wound lesions. J Thromb Haemost. 2006;4:1602–10.
49. Samlaska CR, Winfield EA. Pentoxifylline. J Am Acad Dermatol. 1994;30:603–21.
50. Kaplan AP, Ghebrehiwet B. The plasma bradykinin-forming pathways and its interrelationships with complement. Mol Immunol. 2010;47:2161–9.
51. Korkmaz HI, Ulrich MMW, Wieringen WN, Dogan H, Vlug M, Emmens RW, Meyer KW, Sinige P, Zeerleder S, Wouters D, et al. CI Inhibitor administration reduces local inflammation and capillary leakage, without affecting long-term wound healing parameters, in a pig burn wound model. Antiflamm Antiallergy Agents Med Chem. 2021;20:150–60.
52. Begienemen MP, Kubat B, Ulrich MM, Hahn NE, Stumpf-Stolker Y, Tempelaars M, Middelkoop E, Zeerleder S, Wouters D, van Ham MS, et al. Prolonged CI inhibitor administration improves local healing of burn wounds and reduces myocardial inflammation in a rat burn wound model. J Burn Care Res. 2012;33:544–51.
53. Yang S, Gu Z, Lu C, Zhang T, Guo X, Xue G, Zhang L. Neutrophil extravas- cular traps are markers of wound healing impairment in patients with diabetic foot ulcers treated in a multidisciplinary setting. Adv Wound Care (New Rochelle). 2020;9:16–27.
54. Packard BZ. Artym W, Komoriya A, Yamada KM. Direct visualization of protease activity cells migrating in three-dimensions. Matrix Biol. 2009;28:3–10.
55. Yim N, Ryu SW, Choi K, Lee KR, Lee S, Choi H, Kim J, Shaker MR, Sun W, Park JH, et al. Exosome engineering for efficient intracellular delivery of soluble proteins using optically reversible protein-protein interaction module. Nat Commun. 2016;7:12277.
56. Harmand-Peron E, Juillard F, Saad JS, Roy C, Roinguard P, Summers MF, Darliv JF, Picart C, Muriaux D. Targeting of Murine leukemia virus gag to the plasma membrane is mediated by PI(4,5)P2/PS and a polybasic region in the matrix. J Virol. 2010;84:503–15.
57. Fang Y, Wu N, Gan X, Yan W, Morrell JC, Gould SJ. Higher-order oligomeri- zation targets plasma membrane proteins and HIV gag to exosomes. PLoS Biol. 2007;5:e158.
58. Yuan M, Song ZH, Zhu H, He QJ, Yang B, Sao J. N-mycrotoxylation: from cell biology to translational medicine. Acta Pharmacol Sin. 2020;41:1005–15.
59. Murphy DE, de Jong OG, Brouwer M, Wood MJ, Lavieu G, Schifflers RM, Vater P. Extracellular vesicle-based therapeutics: natural versus engi- neered targeting and trafficking. Exp Mol Med. 2019;51:1–12.
60. Williams EC, Coimbra R, Chan TW, Baird A, Eliceiri BP, Costantini TW. Precious cargo: modulation of the mesenteric lymph exosome payload after hemorrhagic shock. J Trauma Acute Care Surg. 2019;86:62–6.
61. Deskins DL, Ardestani S, Young PP. The polyvinyl alcohol sponge model implantation. J Vis Exp. 2012. https://doi.org/10.3791/3885.
62. Wang X, Ge J, Tredget EE, Wu Y. The mouse excisional wound splinting model, including applications for stem cell transplantation. Nat Protoc. 2013;8:302–9.
63. Veerman RE, Tseuwen L, Czamnevski P, Guduler Akpinar G, Sandberg A, Cao X, Pernemalm M, Ore LM, Gabrielson S, Edlth M. Molecular evaluation of five different isolation methods for extracellular vesicles reveals different clinical applicability and subcellular origin. J Extracellular Vesicles. 2021;10:e12128.
64. Kowal J, Arras G, Colombo M, Jouve M, Morath JP, Primdal-Bengtson B, Dingli F, Leow D, Tkach M, Thery C. Proteomic comparison defines novel markers to characterize heterogeneous populations of extracellular vesicle subtypes. Proc Natl Acad Sci U S A. 2016;113:E968-977.

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