Improved efficiency of heat generation in nonlinear dynamics of magnetic nanoparticles

J. Rácz,1, 2 P. F. de Châtel,3 I. A. Szabó,1 L. Szunyogh,4 and I. Nándori1, 2

1University of Debrecen, H-4010 Debrecen P.O.Box 105, Hungary
2Institute of Nuclear Research, P.O.Box 51, H-4001 Debrecen, Hungary
3MTA-DE Particle Physics Research Group, H-4010 Debrecen P.O.Box 105, Hungary
4Department of Theoretical Physics and MTA-BME Condensed Matter Research Group Budapest University of Technology and Economics, H-1111 Budapest Budafoki 8., Hungary

The deterministic Landau-Lifshitz-Gilbert equation has been used to investigate the nonlinear dynamics of magnetization and the specific loss power in magnetic nanoparticles with uniaxial anisotropy driven by a rotating magnetic field. We propose a new type of applied field, which is "simultaneously rotating and alternating", i.e. the direction of the rotating external field changes periodically. We show that a more efficient heat generation by magnetic nanoparticles is possible with this new type of applied field and we suggest its possible experimental realization in cancer therapy which requires the enhancement of loss energies.

PACS numbers: 75.75.Jn, 82.70.-y, 87.50.-a, 87.85.Rs

I. INTRODUCTION

Nonlinear dynamics of the magnetization in single-domain ferromagnetic nanoparticle systems has received a considerable attention due to a wide range of their applicability such as magnetic resonance imaging, ultrahigh density magnetic data recording, spintronics, ferrofluids and in biomedical engineering, in particular, drug delivery or hyperthermia [4, 5]. Among many forms of hyperthermia, the local induction of heat via magnetic nanoparticles seems a fruitful strategy with promising preclinical results in different cancer modes [1–3]. The unique feature of magnetic nanoparticle hyperthermia is that the energy is transported in the body by means of an ac magnetic field. At present the clinical application is partly limited due to the efficacy of the heat transfer and the poor controllability of temperature parameters [6]. Thus, the study of relaxation mechanisms of magnetic nanoparticles is a very active research field, both in its theoretical and material-science aspects.

Among many controllable parameters, the applied external magnetic field is one of the most easily variable to increase the efficiency of heat generation. Indeed, there is an increasing interest in the literature to consider the case of rotating external magnetic field [7–17] instead of the commonly applied alternating one, see for example [18]. Some of these studies compare the efficiency of the two types of applied fields. For example, in [9], isotropic nanoparticles were considered without taking into account the thermal effects and the alternating applied field was found to be considerably more favourable than the rotating one. However, it was shown in [13] that the effect of thermal fluctuations modifies the results obtained for the alternating field with isotropic nanoparticles and results in a small difference between the heating efficiency of the rotating and alternating applied fields in the limit of small frequency. Let us note, the inclusion of thermal fluctuations only slightly modifies the findings of the rotating field obtained for isotropic nanoparticles without thermal effects [9].

Magnetic anisotropy can also influence this picture, specially in case of the rotating applied field. An important feature of the rotating external field is the presence of stable steady states (precession modes). Independently of the initial positions, the magnetic moments of nanoparticles tend to the steady state and the dissipated energy can be easily calculated. However, for relatively large anisotropy, more than one steady states appear [7]. Thus, one can study the influence of the transition between these modes on the heating [8, 12]. For example, in Refs. [13, 16] the effect of strong anisotropy on the heating efficiency has been studied and its enhancement is shown for large frequencies near the boundary of various regimes of forced precession (steady states) of the parameter space in case of a rotating applied field. Although, it was argued in [16] that thermal fluctuations do not modify the results but the frequencies where the enhancement is observed are too high for a medical treatment, i.e. for hyperthermia. Another example where the presence of uniaxial anisotropy was considered is Ref. [14], where it was shown that in the low-frequency limit, an easy-axis anisotropy turned out to leave unchange (or slightly decrease) the calculated loss power if no transitions between the various precession modes (steady states) are taken into account which is the case for relatively moderate
anisotropy. In summary, the alternating applied field is found to be slightly more favourable for low-frequencies which is suitable for hyperthermia and the small or moderate anisotropy does not change this picture.

Instead of trying to decide whether an alternating or a rotating external magnetic field is more suitable for magnetic nanoparticle hyperthermia, here we propose a new type of applied field, which is "simultaneously rotating and alternating". In particular, we demonstrate that a more efficient heat generation by magnetic nanoparticles is possible if the direction of the rotating external field changes periodically and the particles exhibit a moderate anisotropy. We show results of this new and successful attempt which enhances the loss energy drastically by means of abrupt changes in the applied magnetic field (sudden change of the direction of the rotating field after every circle). The change in the direction of the rotating applied field dislocates the magnetic moment of the nanoparticle out of its steady state, i.e. the precession mode. Since the steady state solution corresponds to minimal dissipation, a more effective heating can be achieved if the system is out of the steady state. We argue that the loss energy achievable by changing the direction of a rotating field is worth to study as a possible tool to enhance the heat in hyperthermia. The calculation has been done for a single, simple configuration, but the stunning result is worth checking experimentally. Indeed, we propose another new type of rotating applied field which has a periodically alternating direction, similarly to the case of "sudden change" studied in the present work but with a feature of being more suitable for experimental realisation.

The paper is organised as follows. In Sec II we discuss the deterministic Landau-Lifshitz-Gilbert equation in case of uniaxial anisotropy with rotating applied field where overall units and parameters suitable for hyperthermia are also considered. Some known results on the specific loss power and loss energy obtained in the steady state solutions of the Landau-Lifshitz-Gilbert equation for oblate (positive anisotropy) particles is summaries briefly in Sec III and new results for prolate (negative anisotropy) particles are discussed. New findings related to the loss energy per cycle out of the steady state are shown in Sec IV. In Sec V we propose a novel type of applied field which is rotating with periodically changed direction. Proposal for experimental realisation of the new applied field is discussed in Sec VI. Finally, Sec VII stands for the summary and a detailed discussion for the optimised set of parameters for magnetic particle hyperthermia is given.

II. LANDAU-LIFSHITZ-GILBERT EQUATION

Out of the many phenomenological equations of motion for the relaxation of magnetization [12] the Gilbert equation [20] has proved to give the one of the most realistic description of the dynamics of single-domain magnetic particles at strong damping (Ref. [2] represents another frequently used approach). Such a particle, being too small to accommodate a domain wall, can be fully characterized with a single vector, its magnetic moment \( \mathbf{m} \). An important feature of Larmor precession is that \( |\mathbf{m}| = m_s \) does not change under the influence of the external field, including the anisotropy field. Hence it is convenient to rewrite the equation of motion of the magnetization \( \mathbf{m} \) of a single-domain particle in terms of the unit vector \( \mathbf{M} = \mathbf{m}/m_s \), \( m_s \) being the saturation magnetic moment (e.g. \( m_s \approx 10^5 \) A/m for single crystal Fe3O4). Then the Gilbert equation reads as

\[
\frac{d}{dt} \mathbf{M} = \gamma_0 \mathbf{M} \times \nabla M V + \mu_0 \eta \frac{d}{dt} \mathbf{M},
\]

(1)

where \( \gamma_0 = 1.76 \times 10^{11} \) Am²/Js is the gyromagnetic ratio of the electron spin (with opposite sign), \( \mu_0 = 4\pi \times 10^{-7} \) Tm/A (or N/A²) is the permeability of free space, \( V \) is the potential energy and \( \eta \) is the damping factor, both of them normalized for unit \( M \). To describe the system, the potential energy must contain the Zeeman energy in the external applied magnetic field and the anisotropy energy [8]

\[
V = -\mu_0 \mathbf{M} \cdot \mathbf{H}_{ext} - \frac{\mu_0}{2} H_0 M_z^2
\]

(2)

where \( M_z \) is the \( z \)-component of the normalized magnetization vector and the external applied field is a rotating one (perpendicular to the anisotropy field)

\[
\mathbf{H}_{ext} = H_0 (\cos(\omega t), \sin(\omega t), 0),
\]

(3)

with the angular frequency \( \omega \). We define the vector \( \mathbf{H}_{eff} \), which contains the external applied magnetic field and the effect of the anisotropy of the magnetic particle

\[
\mathbf{H}_{eff} = -\frac{1}{\mu_0} \nabla M V = -\frac{1}{\mu_0} (\partial M_z, \partial M_z, \partial M_z) V = H_0 (\cos(\omega t), \sin(\omega t), \lambda_{eff} M_z),
\]

(4)

with \( \lambda_{eff} = H_0/H_0 \). Clearly, if \( \lambda_{eff} > 0 \) \( (H_0 > 0) \), the anisotropy will turn the magnetization towards the \( z \)-axis, if \( \lambda_{eff} < 0 \) \( (H_0 < 0) \), into the \( xy \)-plane. Giordano et al. [22] treated the shape anisotropy of the isotropic ellipsoidal particles using a different notation, where \( L \) is the parameter giving the deviation from spherical symmetry. The link to our parameters is \( H_0 = (3L - 1)m_s \). Although, our model does not specify the source of anisotropy, given the material used in hyperthermia, we have to deal with shape anisotropy.

Equation (4) implies a uniaxial anisotropy with a potential energy \( -(\mu_0/2)H_0 \lambda_{eff} M_z^2 \), which has its minima at \( |M_z| = 1 \) for \( \lambda_{eff} > 0 \) and \( M_z = 0 \) for \( \lambda_{eff} < 0 \). Two ellipsoids of revolution have the shapes with the geometry of this energy: for \( \lambda_{eff} > 0 \) oblate (cigar-shape) and for \( \lambda_{eff} < 0 \) prolate (lens shape).

The Gilbert equation (1) can be rewritten in such a way that it has a functional form similar to the Landau-
Lifshitz equation [21]. This is called the Landau-Lifshitz-Gilbert (LLG) equation,

$$\frac{d}{dt} \mathbf{M} = -\gamma'[\mathbf{M} \times \mathbf{H}_{\text{eff}}] + \alpha'[(\mathbf{M} \times \mathbf{H}_{\text{eff}}) \times \mathbf{M}], \quad (5)$$

where \( \gamma' = \mu_0 \gamma_0/(1 + \alpha^2) \) and \( \alpha' = \gamma' \alpha \) with the dimensionless damping factor \( \alpha = \mu_0 \gamma_0 \mu_0 \mathbf{m}_S \). For example, \( \alpha = 0.1 \) was chosen in [16] and \( \alpha = 0.3 \) was used in [22].

Writing Eq. (5) in polar coordinates \((M, \theta, \phi)\) allows to drop the constant \((\mathbf{M})\), leaving but two equations:

$$\frac{d\theta}{dt} = \omega_L \sin \phi + \alpha_N \cos \theta \cos \phi - \alpha_N \lambda_{\text{eff}} \sin \theta \cos \theta,$$

$$\frac{d\phi}{dt} = \omega_L \cos \phi \cos \theta + \omega - \alpha_N \sin \phi \sin \theta - \omega_L \lambda_{\text{eff}} \cos \theta \quad (6)$$

where \( \omega_L = H_0 \gamma' \) and \( \alpha_N = H_0 \alpha' \). Note that (6) is written in a new coordinate system rotating with the applied field: the azimuthal angle \((\phi)\) has been cut into the rotation \((\omega t)\) and a measure \((\phi)\) of the lag of \(\mathbf{M}\) with respect to the rotation of the applied field: \(\varphi = \omega t - \phi\).

Knowing that in the practice \( H_0 \approx 18 \) kA/m we find that \(\omega_L\) is of the order of \(10^9\) Hz. In hyperthermia the frequency of the applied field is advised to be chosen between \(10^5\) and \(5 \times 10^5\) Hz, so that \(\omega\) is four orders of magnitude below \(\omega_L\). Furthermore, \(\alpha_N = \alpha \omega_L\). For example, a set of parameters of [6] typical for hyperthermia (with \(\alpha = 0.1\) and \(H_0 = 18\) kA/m),

\[
\omega = 5 \times 10^5 \text{Hz}, \quad \omega_L = 4 \times 10^8 \text{Hz}, \quad \alpha_N = 4 \times 10^8 \text{Hz},
\]

and the dimensionless anisotropy parameter \(\lambda_{\text{eff}}\) depends on the shape and geometry of the nanoparticle. The left sides of (6) being derivatives of angles with respect to time, the units of all terms in the equations must be \(s^{-1}\).

Their dimension can be taken of introducing a dimensionless damping factor \(\gamma = \mu_0 \gamma_0 \mu_0 \mathbf{m}_S \). For example, (6) is being cut into a single cycle, \(t = t_0\) where \(t_0 = 0.5 \times 10^{-15}\) s is chosen in this work, thus, e.g. the dimensionless form of (6) reads

\[
\omega \rightarrow \omega t_0 = 2.5 \times 10^{-5},
\]

\[
\omega_L \rightarrow \omega_L t_0 = 0.2,
\]

\[
\alpha_N \rightarrow \alpha_N t_0 = 0.02.
\]

Let us note, \(t_0\) is chosen to be in the range of the attempt time \(\tau_0\) used in Neel relaxation. Typical values for \(\tau_0\) are between \(10^{-10}\) and \(10^{-9}\) seconds.

III. STEADY STATE SOLUTION OF THE LLG EQUATION

The solution of Eq. (6) is shown in Fig. 1 for a particular set of (dimensionless) parameters given in the caption. As expected below the critical value of the anisotropy \(\lambda_{\text{eff}} < \lambda_c\), only a single attractive fixed point appears [14], which corresponds to a steady state solution of the original LLG equation (5) (single periodic precession mode),

\[
M_x(t) = u_{x0} \cos(\omega t) - u_{y0} \sin(\omega t),
\]

\[
M_y(t) = u_{x0} \sin(\omega t) + u_{y0} \cos(\omega t),
\]

\[
M_z(t) = u_{z0}.
\]

where \(u_{x0}\) and \(u_{y0}\) are determined by \(\omega, \omega_L, \alpha_N\) and \(\lambda_{\text{eff}}\). The loss energy is calculated using these attractive fixed point solutions in the formula for the energy dissipated in a single cycle,

\[
E = \mu_0 m_S \int_0^{2\pi} dt \left( \mathbf{H}_{\text{eff}} \cdot \frac{d\mathbf{M}}{dt} \right)
\]

\[
= \mu_0 2\pi m_S H_0 (-u_{y0}), \quad (10)
\]

(see also Eq.(12) in [14]) which has the following form in the low-frequency \(\omega \ll \alpha_N\) and small anisotropy \(|\lambda_{\text{eff}}| \ll 1\) limits

\[
E \approx 2\pi \mu_0 m_S H_0 \left[ \frac{\alpha_N \omega}{\omega_L^2 + \alpha_N^2} - \frac{\alpha_N \omega^2 \omega_0^2}{(\omega_L^2 + \alpha_N^2)^3} \left( 1 + 2 \lambda_{\text{eff}} \right) \right]. \quad (11)
\]

It is clear that for positive (negative) \(\lambda_{\text{eff}}\) the energy per cycle is decreased (increased) by the anisotropy albeit for relatively large frequencies. Since \(\lambda_{\text{eff}}\) appears only at the next-to-leading terms, if one takes the low-frequency limit \((\omega \rightarrow 0)\) the effect of anisotropy is irrelevant. This result has been discussed in [14] and can be seen in Fig. 2, which shows that for \(|\lambda_{\text{eff}}| \ll \lambda_c\), and for small frequencies, the loss energy per cycle becomes identical to that in the isotropic case, independently of the sign of \(\lambda_{\text{eff}}\).
For large anisotropy, $|\lambda_{\text{eff}}| > \lambda_c$, (if no transition between the various precession modes is taken into account) the loss energy per cycle tends to zero for $\lambda_{\text{eff}} > 0$, and to a constant (almost identical to the isotropic value if $\omega \to 0$) for $\lambda_{\text{eff}} < 0$. Similar observation holds for the loss energies in the steady states which exist only above the critical anisotropy, see the dashed lines in Fig. 2. For low frequencies, the dashed lines tend to zero for $\lambda_{\text{eff}} > 0$ and to a constant for $\lambda_{\text{eff}} < 0$. As to the application in hyperthermia, these results confirm that particles of lens shape provide an enhanced loss energy, but at the allowed frequency the effect is not significant. It is important to note that frequencies ($\omega = 0.01 - 0.15$) shown in Fig. 2 are too large for biomedical application.

IV. LOSS ENERGY PER CYCLE OUT OF THE STEADY STATES

Up to now, we studied the loss energy per cycle calculated at the steady state solution of the LLG equation (i.e. at the attractive fixed point of Fig. 1). However, it is a relevant question to address whether one can find a larger loss energy in a single cycle if it is calculated out of the steady states. Indeed, in the 3D-plot of Fig. 3 we show the loss energy obtained in the first cycle of the external field as a function of various starting points on the $(\theta, \phi)$ plane. Note that in the low-frequency limit (suitable for hyperthermia), the solution of the LLG equation always tends to the attractive fixed point very rapidly, i.e. it reaches the fixed point with one percent accuracy in a quarter of a full circle. In Fig. 3 the "well" corresponds to the attractive fixed point which produces us the lowest loss energy per cycle while the "hill" where the loss energy is the maximum is related to initial conditions taken at the repulsive fixed point. Though, the results displayed in Fig. 3 are obtained numerically, an approximate analytic derivation is possible for the isotropic case ($\lambda_{\text{eff}} = 0$). Indeed, an approximate solution to the LLG equation is given by Eq. (29) of [9] which reads

$$M_x(t) = M_{\text{spec}} \cos(\Omega t) - M'^{\text{spec}} \sin(\Omega t) + (M_{\xi 0} - M_{\text{spec}}) e^{-\frac{\alpha_N t}{2}},$$

$$M_y(t) = M_{\text{spec}} \sin(\Omega t) + M'^{\text{spec}} \cos(\Omega t) + (M_{\eta 0} - M'^{\text{spec}}) e^{-\frac{\alpha_N t}{2}},$$

$$M_z(t) = \sqrt{1 - [M_x(t)]^2 - [M_y(t)]^2},$$

(12)

where $(M_{\xi 0}, M_{\eta 0}, M_{\zeta})$ represents the magnetization vector in a particular rotated coordinate system and depends on the initial values of the cartesian coordinates $M_{\xi 0}$ and $M_{\eta 0}$ linearly. $(M'^{\text{spec}}, M'^{\text{spec}})$ depend on the parameters $\omega, \omega_L, \alpha_N$ defined by Eq. (28) of [9] and $\Omega = \sqrt{\omega^2 + \omega_L^2}$. According to (10), the loss energy per cycle has a linear dependence on the initial cartesian coordinates $M_{\xi 0}$ and $M_{\eta 0}$ as well. Thus, rewriting them by polar coordinates

$$M_{\xi 0} \propto \sin(\theta) \cos(\phi), \quad M_{\eta 0} \propto \sin(\theta) \sin(\phi)$$

(13)

one finds

$$E/(1\text{st cycle}) = A \sin(\theta) \cos(\phi) + B \sin(\theta) \sin(\phi)$$

(14)

where $A, B$ constants depend on the parameters $\omega, \omega_L, \alpha_N$ which is in agreement to the numerical result of
As a new idea let us consider the loss energy per cycle in case of a rotating applied magnetic field where the direction of rotation is changed periodically, i.e., after every full cycle the sign of $\omega$ is switched in Eq. (14). By changing the direction, the position of the steady state solution is changed, i.e. for $\omega > 0$ ($\omega < 0$) it is below (above) the equator of the orbit map. Thus, the magnetization vector always tends from a disappearing steady state to an arising one. Note that we do not calculate this effect above $\lambda_c$ because in that case more than one stable steady state solutions appear. The outcome is plotted in Fig. 2 with dotted lines.

For high frequencies ($\omega = 0.15$ and $\omega = 0.1$), irrelevant to the sign of $\lambda_{\text{eff}}$, there is an increase in the loss energy, tending to constant values close to $\lambda_c$. The effect is larger for $\lambda_{\text{eff}} > 0$, because in this case the positions of the steady state solutions (for $\omega < 0$ and $\omega > 0$) are far from each other.

For low frequencies ($\omega = 0.001$) the situation completely changes as the loss energy for $\lambda_{\text{eff}} > 0$ becomes larger than any other calculated values, including those found for $\lambda_{\text{eff}} < 0$. For example, for lower values of the damping, i.e. $\alpha_N = 0.05$ or $\alpha_N = 0.01$ the loss energy monotonously increases with $\lambda_{\text{eff}}$, reaching a value that is about 15% or 100% larger as compared to the isotropic case near (below) $\lambda_c$, see Fig. 4. Therefore, a more efficient heat generation is possible for physical values of the damping (i.e. for $\alpha = 0.1 - 0.3$ where $\alpha_N = \alpha \omega_L \approx 0.02 - 0.06$), near the critical anisotropy $\lambda_{\text{eff}} = \lambda_c \approx 1$ if the direction of the rotating applied field is changed periodically. In summary, the reason for the peaks of the dissipated energy at $|\lambda_{\text{eff}}| = 1$ in Fig. 4 (dotted lines) is twofold: (i) it was shown that a more effective heating can be achieved if the system is out of the steady state which is achieved by the new type of applied field (dotted lines) which is simultaneously rotating and alternating, (ii) this enhancement effect becomes larger at $|\lambda_{\text{eff}}| = 1$ where the system is close to the critical anisotropy $|\lambda_c| = 1$, where the dislocating effect caused by the change in the direction of the rotation is the largest.

![Graph](image)

**V. ROTATING FIELD WITH PERIODICALLY CHANGED DIRECTION**

![Graph](image)

**FIG. 4: The loss energy per cycle as a function of the anisotropy parameter $\lambda_{\text{eff}}$ is shown for various values of $\alpha_N$ (for fixed $\omega$ and $\omega_L$).**

**VI. PROPOSAL FOR EXPERIMENTAL REALIZATION**

Finally, let us propose a new type of "rotating" applied field which has a periodically alternating direction, similarly to the case carefully analyzed above but with a feature of being more suitable for experimental realization. Nonetheless, a "sharp change" in the direction of the rotating field which is studied previously is also feasible in practice. Our proposal for the applied field is

$$H_{\text{eff}} = H_0 (\cos(2\omega t), \sin(\omega t), \lambda_{\text{eff}} M_z),$$

(15)

where the $2\omega$ of the cosine naturally provides us with the required change in the direction in every half cycle. Well separated and oriented anisotropic nanoparticles in an aerogel matrix can serve as a good experimental setup to realize the enhanced loss energy in case of an applied field as in Eq. (15). The practical advantage of (15) is that it requires the use of two frequencies $\omega$ and $2\omega$ and no higher harmonics or no rapid switchings are needed. Of course, one has to choose the frequency $\omega$ in a way that $2\omega$ should be in the range suitable for hyperthermia.

**VII. SUMMARY**

In this work we showed that a more efficient heat generation by magnetic nanoparticles is possible if the direction of the rotating external field changes periodically. We would like to emphasise that the heating efficiency of the new type of applied field is larger than those of the rotating and alternating ones which are almost identical in the limit of small frequency, see for example [11, 13]. Based on this finding, we make a proposal to apply a magnetic field regularly stopping its rotation,
which should increase the loss energy. Conditions used in the proposed work towards an enhance of heating efficiency are the followings.

**Applied field.**—A new type of “rotating” applied field is proposed here which has a periodically alternating direction either using the form \[\omega \text{ where } \omega \text{ is assumed to change sign in every full circle or using }\]

\[\text{ where } 2\omega \text{ of the cosine naturally provides us with the required change in the direction in every half cycle. The frequency is in the range of hyperthermia, }\]

\[\text{ is in the range of hyperthermia, }\]

\[\text{ is in the range of hyperthermia, }\]

\[\text{ which should increase the loss energy. Conditions used in the proposed work towards an enhance of heating efficiency are the followings.}\]

**Anisotropy.**—The nanoparticles are assumed to be oblate ellipsoids where the shape anisotropy is moderate, i.e. \(\lambda_{\text{eff}} = H_\alpha/H_\Omega \approx 1\) (which implies \(L = 1.2/3 = 0.4\) according to Ref. 22 for \(H_\alpha = 0.2 \times 10^5\text{A/m and }M_\alpha = 10^9\text{A/m}\)). In this case the nanoparticle has a single precession mode. However, for larger anisotropy, i.e. \(\lambda_c < \lambda_{\text{eff}}\) which has been discussed in 16 (where \(\tilde{h} = \lambda^{-3/2}\)) more than one precession modes appear. In Ref. 16 an enhancement of the heating efficiency was found near the boundary of these regimes of forced precession. The largest increase is observed between the periodic and quasi-periodic regimes, however, it exists only for large values of the reduced frequency used in 16 which is not allowed in hyperthermia. Nevertheless, it is expected that in case of an applied field, Eq. 15 which can be considered as a rotating field (with alternating direction) where the magnitude changes slightly, the effect of the increased upward heating becomes even stronger due to the transition between the two periodic modes. Finally, let us note that regarding the anisotropy, one has to take into account the structure formation and synchronization of interacting magnetic nanoparticles which have been studied e.g., in 23 for rotating fields.

**Orientation.**—The anisotropy field (shape anisotropy caused by oblate particles) is assumed to be perpendicular to the plane where the applied field rotates. In practice, this special situation can be achieved by switching on a strong static field which orients all the nanoparticles and than the rotating field applied while the static field switched off. For an appropriate size of the nanoparticle (with an average diameter \(d = 14\text{nm}\)) the orientation of the major part of the nanoparticles remains unchanged (for long enough time) and only the magnetic moment has a dynamics under the rotating field. Number of parameters (for example biomedical coating) can be tuned in order to design the nanoparticles (see e.g. 20) for biomedical application incorporating the requirement for particle size and shape-anisotropy. Furthermore, in 16 it was argued that if the average diameter is chosen to be in the range \((d_{\text{min}}, d_{\text{max}})\) than the nanoparticles have single-domains and one finds no restriction on the applied frequency and their dynamics is almost deterministic. The boundary values, \(d_{\text{min}}\) and \(d_{\text{max}}\) depend on the parameters such as the anisotropy factor: e.g., in case of relatively large anisotropy \((\tilde{h} = 0.1)\) one finds \(d_{\text{min}} = 13.7\text{nm}\). Thus, our choice \(d = 14\text{nm}\) indicates that the description of the dynamics of the nanoparticle magnetic moments by the deterministic LLG equation is well justified 16 and it is expected that they retain their orientation for long enough time 23.

**Damping.**—The dimensionless damping constant is chosen to be in the range \(\alpha = 0.1 - 0.3\) which was used in the works 16, 22. Accordingly, the enhancement effect shown in this work is 100% - 15% (in case of a smaller damping the enhancement is larger).

---

**Acknowledgement**

This work was supported by the project TÁMOP-4.2.2.A-11/1/KONV-2012-0036 co-financed by the European Union and the European Social Fund. Partial support is acknowledged to the Jnos Bolyai Research Scholarship of the Hungarian Academy of Sciences and to the National Research, Development and Innovation Office of Hungary under project No. K115575.

---

[1] C. Scherer, H.G. Matuttis, Phys. Rev. E 63 011504 (2000); J. Embs, H. W. Müller, C. Wagner, K. Knorr, and M. Lücke, Phys. Rev. E 61, R1916 (2000); B. U. Felderhof, Phys. Rev. E 62, 3848 (2000); M.I. Shliomis, Phys. Rev. E 64, 063501 (2001); B. U. Felderhof, Phys. Rev. E 64, 063502 (2001); H.W. Müller and M. Liu, Phys. Rev. E 64, 061405 (2001); J. P. Embs, S. May, C. Wagner, A. V. Kityk, A. Leschhorn, and M. Lücke, Phys. Rev. E 73, 036302 (2006); A. Leschhorn, M. Lücke, C. Hoffmann and S. Altmayer, Phys. Rev. E 79, 036308 (2009).

[2] M.I. Shliomis, Zh. Eksp. Teor. Fiz. 61, 2411 (1971) [Sov. Phys. JETP 34, 1291 (1972)]; M.I. Shliomis, Usp. Fiz. Nauk 112, 427 (1974) [Sov. Phys. Usp. 17, 153 (1974)]; R.E. Rosensweig, Ferrohydrodynamics, Cambridge University Press, Cambridge, (1985); M.I. Shliomis, Phys. Rev. E 64, 060501(2001); R.E. Rosensweig, Ferrohydrodynamics, Cambridge University Press, Cambridge, (1985); M.I. Shliomis, Phys. Rev. E 64, 060501(2001).

[3] Q. A. Pankhurst, J. Connolly, S. K. Jones, and J. Dobson, J. Phys. D: Appl. Phys. 36, R167 (2003); M. Ferrari, Nat. Rev. Cancer 5, 161 (2005); R. Hergt, S. Dutz, R. Muller, M. Zeisberger, J. Phys.: Condens. Matter 18 S2919 (2006); R. Hergt, S. Dutz, J. Magn. Magn. Mater. 311, 187 (2007); S. Laurent, D. Forge, M. Port, A. Roch,
C. Robic, L. Vander Elst, and R. N. Muller, Chem. Rev. 108, 2064 (2008); J. D. Alper, Thesis (Ph.D.), Massachusetts Institute of Technology (2010); Quian Wang and Jing Liu, Fundamental Biomedical Technologies 5, 567-598 (2011), Springer Science+Business Media: Interacellular Delivery (ed. A. Prokop); A. L. E. Rast, Thesis (Ph.D.) University of Alabama, Birmingham (2011); D. E. Bordelon, C. Cornejo, C. Grüttnner, F. Westphal, T. L. DeWese, R. Ivkov, J. Appl. Phys. 109, 124904 (2011); M. V. Petrova, et al., Applied Magnetic Resonance 41, 525 (2011); A. Arakaki, K. Shibata, T. Mogi, M. Hosokawa, K. Hatakeyama, H. Gomyo, T. Taguchi, H. Wake, T. Tanaka, T. Matsunaga and T. Tanaka, Polymer Journal 44, 672 (2012). S Bucak, B Yavuztürk, A D Sezer, Recent Advances in Novel Drug Carrier Systems, Ali Demir Sezer (Ed.), ISBN: 978-953-51-0810-8, InTech. (2012)