Surgical treatment of Achilles tendon rupture
Examination of strength of 3 types of suture techniques in a cadaver model

Robbert A Zandbergen¹, Stefan F de Boer¹, Bart A Swierstra¹, Judd Day¹, Gert-Jan Kleinrensink² and Annechien Beumer¹

Departments of ¹Orthopedic Surgery and ²Anatomy, Erasmus University Medical Center, Rotterdam, The Netherlands
Correspondence BAS: b.swierstra@maartenskliniek.nl
Submitted 03-04-11. Accepted 04-03-31

Background The mechanical properties of present-day percutaneous repairs of Achilles tendon ruptures are not known.

Material and methods Artificially-created ruptures in 24 human cadaveric Achilles tendons were repaired with an open Bunnell repair, a percutaneous calcaneal tunnel or a percutaneous bone-anchor repair. In the open technique no.1 PDS-II absorbable suture material was used, and in the percutaneous techniques either no.1 PDS-II or no.1 Panacryl absorbable suture material was used. The specimens were tested in a materials testing machine until failure occurred.

Results The common mode of failure was suture breakage in non-anchor repairs, and anchor pullout in anchor repairs. The average strength of the repairs varied from 166 N (SD 60) to 211 N (SD 30), with no differences between the techniques (p = 0.5).

Interpretation Taking costs into account, the percutaneous calcaneal tunnel technique and the open technique are the methods of choice.

Various procedures have been described for the treatment of acute Achilles tendon rupture. Before the 1980s, nonoperative treatment was the most common approach (Nistor 1981). Recent studies have suggested that surgical treatment may have advantages over nonsurgical treatment (Möller et al. 2001, Wong et al. 2002), and that percutaneous repairs are preferable to open procedures (Lim et al. 2001). There have been very few mechanical studies regarding differences in strength of the various types of surgical Achilles tendon repair (Hockenbury and Johns 1990, Mortensen and Saether 1991, Watson et al. 1995, Cretnik et al. 2000, Jaakkola et al. 2000).

We have assessed the strength of a percutaneous bone-anchor repair and a calcaneal tunnel repair, and have compared these to the strength obtained from the classical open repair for acute Achilles tendon rupture. We also compared the strength of 2 different bioresorbable suture materials, monofilament PDS-II and braided Panacryl, for use in the repairs.

Materials and methods
Free suture tests
To assess the strength of commonly used suture material, we tested single-strand no.1 PDS-II and Panacryl (Johnson & Johnson, Brussels, Belgium) in a screw-driven Lloyd Instruments LRX test machine (Lloyd Instruments, Hampshire, UK). The sutures were tested in a loop set-up. The loop was closed with 8 alternating knots; it was 20 cm long. The sutures were preconditioned for 20 cycles at a rate of 6 mm/s up to 30 N, followed by a linear extension done at 6 mm/s until failure occurred. A preload of 2 N was maintained between the cycles. Each test was repeated 5 times. Force and extension were measured and recorded by computer.
Tendon tests

We used 24 fresh-frozen human cadaveric lower legs with a mean age of 79 (SD 12) years. A bone-tendon unit consisted of the Achilles tendon with a part of the os calcis. A simulated rupture was made by a sharp cut through the tendon 4 cm cranial to the calcaneal insertion.

The tendons were repaired by one of the following methods: 1. open technique: 2 PDS-II no.1 (n = 5), 2. percutaneous calcaneal-tunnel technique: 2 PDS-II no.1 (n = 4), 3. percutaneous calcaneal-tunnel technique: 2 Panacryl no.1 (n = 5), 4. percutaneous repair: 2 Mitek anchors and 2 PDS-II no.1 (n = 5), 5. percutaneous repair: 2 Mitek anchors and 2 Panacryl no.1 (n = 5).

In the open repair group, the tendon parts were sutured using the Bunnell method (Figure 1a). For the percutaneous repairs, the Bunnell method was used for the proximal intra-tendineous part. In the calcaneal tunnel groups (2 and 3), a 2.0-mm hole was drilled transversely through the calcaneus and the sutures were transported through the tunnel in the calcaneus using a suture retriever (Figure 1b).

In the bone anchor groups (4 and 5), 2 bone anchors were used. The anchors were placed according to the instructions of the manufacturer (Figure 1c). All repairs had 4 strands of suture material passing from the distal part of the tendon to the proximal part, which were tied together with 8 alternating knots.

The repaired bone-tendon units were put into the LRX testing machine, with the os calcis fixed in a bone clamp with 6 screws and the tendon in a tendon clamp. Both clamps were custom-made (Figure 2). The LRX-crosshead speed was set at 6 mm/s for detailed recording of force and extension data. The specimens were preconditioned 20 times with a preload of between 2 N and 30 N, followed by a linear extension until failure. Between the cycles, a preload of 2 N was maintained. Failure was defined as either breaking of the suture, tendon rupture, anchor pullout, or calcaneal tunnel failure. Force and crosshead displacement were recorded. Force-displacement curves and ultimate load were assessed in order to compare the different methods.

Statistics

Because of the small numbers of specimens per group, statistical analysis was performed with a nonparametric one-way ANOVA of all groups (Kruskal-Wallis and Mann-Whitney test), with the significance level set at $p \leq 0.05$ (Jandel Sigma Stat 2.0 statistics package, SPSS Inc., Chicago, IL). The statistical power, assuming 30% minimal relevant difference, was approximately 80%.
Results

Free suture test

The mode of failure was suture breakage at the knot. The average strength in a two-strand set-up of PDS-II was 96 N (SD 9.2), and that of Panacryl was 99 N (SD 5.7). There was no difference in strength (p = 0.4). Up to a load of 50 N, PDS-II showed more lengthening than Panacryl, with a compliance of 0.41 mm/N (SD 0.02) as opposed to 0.19 mm/N (SD 0.03) (p = 0.008). The Panacryl wire yielded after a load of 53 N.

Tendon tests

In the 5 open repairs the suture broke in 4 cases, while in 1 case the intact suture was ripped out of the tendon. Failure in the 9 tunnel repairs occurred at the suture in 8 cases. In 1 case, the tunnel itself failed. In 9 of 10 anchor repairs, the failure was anchor pullout. Suture breakage was seen once. No differences in strength were found between the different repair techniques (p = 0.5) (Table 1).

Discussion

The failure strength of the free suture strands in our study corresponded with the manufacturer’s values (personal communication). We found the Panacryl and PDS-II sutures to be of equal strength, but there was a difference in compliance up to a load of 50 N. This may have some influence on the amount of distension between the tendon ends during loading, and should be the subject of further study.

All the anchors were positioned according to the manufacturer’s instructions. Even so, all but one of the anchor repairs failed through pullout of the anchor. This might be due to the high age of the donors. In senile osteopenia, the amount of trabecular and cortical bone is reduced (Simon 1994). It is known that the amount of osteoporosis of the calcaneus corresponds to the overall bone condition of the patient (Wehrli et al. 2002). We did not assess bone mineral density, but as most of the specimens were old, we can assume that osteoporosis in the calcaneus was present. Failure strength of bone anchors depends on cortical bone thickness (Roth et al. 1998). The manufacturer could not supply us with pullout data for this type of anchor. Thus, it may be advisable not to use bone anchors in elderly and osteoporotic patients.

Another possible explanation for anchor failure in the anchor repair groups could be that forces are unequally distributed over both anchors. The tightest loop-anchor combination will sustain most of the load, and will therefore be pulled out first. The bone anchors cost approximately EUR 185 each. One repair requires 2 anchors, which makes this repair more expensive than the other repairs in the study.

This is the first cadaveric study to test the percutaneous calcaneal tunnel technique. The failure strengths found for this repair are comparable with the results of other studies in which 4 suture strands were used (Table 2).

We used the open Bunnell repair as the golden standard to which we could compare the other repairs. The suture was the weakest link in the open Bunnell and in the calcaneal tunnel groups. The strength of the repair benefits from more suture strands crossing the rupture (Table 2). As tested by Jaakkola et al. (2000), the triple-bundle technique with 6 strands showed a higher loading capacity. However, using more suture strands might compromise the tendon or the wound healing.

Although rehabilitation after Achilles tendon repair was not the subject of our study, our advice would be to protect the repair during early mobilization. During walking, the load on an Achilles tendon is around 1430 N (SD 500) for a person weighing 70 kg (Finni et al. 1998). During running, this can rise to 5740 N (Scott and Winter 1990). Both loads are many times greater than the strength of our repairs.

In conclusion, we found the repairs that we studied to be of equal strength. It would not be advisable to use bone anchor repairs for elderly and

| Group | Repair method/ material | n   | Strength (N) mean | SD  | range  |
|-------|-------------------------|-----|-------------------|-----|--------|
| 1     | Open / PDS-II           | 5   | 211              | 30  | 175–242|
| 2     | Tunnel / PDS-II         | 4   | 195              | 33  | 146–217|
| 3     | Tunnel / Panacryl       | 5   | 186              | 26  | 142–209|
| 4     | Anchor / PDS-II         | 5   | 185              | 13  | 169–202|
| 5     | Anchor / Panacryl       | 5   | 166              | 60  | 106–242|
osteoporotic patients. Taking costs into account, the percutaneous calcaneal tunnel technique or the open technique may be preferable. The clinical implications of the various repairs were not studied, and thus no repair can be advocated as being 'the best'. The forces on the Achilles tendon during walking and running exceed the strength of all repairs by manyfold; thus, careful postoperative treatment is imperative.

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Table 2. Overview of mechanical studies of Achilles tendon repair

| No. of strands | Technique | Suture material | Failure (N) | Author          |
|----------------|-----------|-----------------|-------------|----------------|
| 2              | Mason     | Ticron-O        | 45          | Mortensen (1991) |
| 2              | Bunnell   | Ticron-O        | 78          | Mortensen (1991) |
| 2              | Kessler   | Ethibond no. 1  | 85          | Watson (1995)   |
| 2              | Bunnell   | Ethibond no. 1  | 93          | Watson (1995)   |
| 2              | Ma & Griffith | Vicryl no. 2   | 111         | Cretnik (2000)  |
| 4              | Locking loop | Ethibond no. 1 | 147         | Watson (1995)   |
| 4              | Locking loop | Ethibond no. 1 | 161         | Jaakkola (2000) |
| 4              | Modified Ma | Vicryl no. 2   | 214         | Cretnik (2000)  |
| 6              | CSSS *     | Ticron-O        | 175         | Mortensen (1991) |
| 6              | Triple bundle | Ethibond no. 1 | 453         | Jaakkola (2000) |

*CSSS continuous six-strand suture.