Metaplastic and energy-efficient biocompatible graphene artificial synaptic transistors for enhanced accuracy neuromorphic computing

CMOS-based computing systems that employ the von Neumann architecture are relatively limited when it comes to parallel data storage and processing. In contrast, the human brain is a living computational signal processing unit that operates with extreme parallelism and energy efficiency. Although numerous neuromorphic electronic devices have emerged in the last decade, most of them are rigid or contain materials that are toxic to biological systems. In this work, we report on biocompatible bilayer graphene-based artificial synaptic transistors (BLAST) capable of mimicking synaptic behavior. The BLAST devices leverage a dry ion-selective membrane, enabling long-term potentiation, with ~50 aJ/µm² switching energy efficiency, at least an order of magnitude lower than previous reports on two-dimensional material-based artificial synapses. The devices show unique metaplasticity, a useful feature for generalizable deep neural networks, and we demonstrate that metaplastic BLASTs outperform ideal linear synapses in classic image classification tasks. With switching energy well below the 1 fJ energy estimated per biological synapse, the proposed devices are powerful candidates for bio-interfaced online learning, bridging the gap between artificial and biological neural networks.

As the world becomes more interconnected and data-driven, effective deployment of data-intensive computation methods becomes more critical. Large and complex data structures require constant extrapolation, interpolation, and classification, which are ill-suited for memory-constrained von Neumann architectures. A promising approach for overcoming the power and latency shortfalls of traditional computing is through massively parallel neuromorphic systems. A wide variety of devices have been proposed to build such systems, from mature technologies such as metal-oxide and phase change memories to emerging devices such as electrochemical and magnetic memories. Most of these systems, however, employ rigid materials, making them less suited for direct integration with biological matter. Direct interfacing of artificial neuromorphic systems with biological living neurons is a highly ambitious goal, which in the long term may lead to effective brain implants and creation of artificial tissue. There have recently been device innovations to this end utilizing organic materials such as maltose-ascorbic acid, zein, PVA, and cellulose but with various deficiencies in synaptic performance. Two-dimensional (2D) materials are a promising material class for bioelectronics and neuromorphics due to their unique electronic properties and atomically thin structure, allowing for imperceptible interfacing with tissue. However, existing 2D-material based...
neuromorphic systems often employ elements that would induce toxicity when interacting with biological systems, e.g., involving elements like Li+ ionic carriers22,23 which directly impact the nervous system34. Other 2D carbon-based systems have non-ideal conductance responses that negatively impact performance in neuromorphic applications21-27. As a result, new device innovations are needed for future neuromorphic computing solutions that can directly integrate with biological tissue.

The biocompatible graphene-based artificial synaptic transistors (BLAST) introduced in this work are a combination of two flexible, soft, and biocompatible elements: Nafion and graphene. Nafion plays the role of a solid polymeric electrolyte made of a negatively charged polysulfonated backbone28 with mobile islands of positively charged water/proton clusters (Fig. 1a). When Nafion is in an environment with a high concentration of protons, channels are formed in the material matrix, allowing for high mobility transport of protons28. In contrast, when there is a low concentration of protons, the protonic charge carriers exist in the form of semi-mobile clusters20. When a current pulse is applied through the Nafion, we hypothesize that the positively charged clusters move in the opposite direction of electron current and provide an effective change in the local electrical double layer (EDL) at the Nafion-graphene interface, yielding high-precision conductance states for synaptic operation in artificial neural networks. Altogether, the proposed devices feature favorable synaptic characteristics and energy efficiency down to 50 aJ/µm2. We evaluate this behavior through neuromorphic simulations on several classification tasks using a prototypical neural network and show that the BLAST devices feature metaplasticity that allows online learning performance exceeding ideal linear, numerical synapse results.

**Results**

In this work, two kinds of BLAST devices were fabricated: macroscale (mBLASTs, 10–100 mm² in area) and microscale (μBLASTs, ~400 µm² in area). The mBLASTs were fabricated using 180 µm thick Nafion-117, adhesive conductive gold tape to form source and drain electrodes, and graphene electronic tattoos31,32 supported by 200 nm thick PMMA (details in Methods). It is important to note here that both graphene and Nafion are known to be biocompatible substrates for cellular interfaces. Since a few decades of its discovery, Nafion has been studied for biocompatibility as a bare substrate and has also been widely accepted as a coating material for numerous in vivo biosensing applications33-35. Graphene, despite the original claims of cytotoxicity, has gained trust in the biomedical research community as a highly biocompatible substrate. Unlike the nm-sized flakes of exfoliated graphene, CVD-grown monolayer graphene supported by a substrate is known to not alter any cellular function36, and often serves as an advantageous substrate for cell growth7-30. To make mBLASTs, we leverage the previously developed large-scale graphene electronic tattoos (GETs) that are transferred on top of the Nafion, self-adhering and forming a tight interface between the graphene and Nafion. The water-assisted transfer, though rapid (<10 s), leads to hydration of the Nafion membrane; hence the used Nafion cannot be considered completely dry, leading to relatively increased mobility of proton clusters29. The fabricated devices, as shown in Fig. 1a, are highly flexible and transparent. The average bilayer graphene channel width is 4 mm, and length 3–5 mm, yielding an average area of 15 ± 2 mm². In a separate experiment, we varied the area of mBLAST devices and recorded the change in properties. The gold electrode used to apply synaptic gate potential through the Nafion typically outsizes the graphene interface itself to ensure that the whole graphene-Nafion interface is

![Image](https://via.placeholder.com/150)

**Fig. 1** | **BLAST configuration and functionality.** *a* Photograph of a transparent BLAST device. *b* 3D schematic of the BLAST device showing source (S), drain (D), and gate (G) electrodes. *c* Cross-sectional schematic of BLAST device operation in high and low conductance states. Nafion (teal) contains mobile positively charged clusters of protons (dark red) carried through the membrane; source, drain, and gate gold contacts are shown in yellow with source grounded. The pre-synaptic write pulse is labeled Iₚ, and the corresponding post-synaptic read current change is labeled Iᵣ. Applied post-synaptic voltage (green) is labeled Vₛ. *d* Measured BLAST conductance vs. time as the gate current is periodically pulsed, showing distinct and repeatable conductance levels. The color/direction and length of the depicted pulses represents the sign and relative amplitude of the applied pulse, respectively. *e* Transfer characteristics with forward and reverse sweep at various sweep rates (11 mV/sec – blue, 55 mV/sec – green, and 110 mV/sec – yellow). Solid lines represent drain-source current; Dashed lines represent gate-source current. *f* Performance for positive and negative trainings of 20 write pulses each while gradually increasing current pulse amplitudes from 1 µA (black) to 10 µA (yellow) for 1 ms duration, showing that conductance weights can be modulated by the gate-source current and desired synaptic characteristics of high symmetry and linearity.

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used effectively. The device schematics and cross-section can be seen in Fig. 1b, c and additional schematic details can be found in Supplementary Fig. 1. The channel conductance of the synaptic device increases in response to negative current pulses applied through the Nafton membrane and decreases in response to positive current pulses, with the amplitude of conductance change correlating with the amplitude of applied pulse (Fig. 1d). The response is symmetrical, reversible, and scalable.

We hypothesize that positive (negative) current pulses cause the semi-mobile positively charged proton-concentrated clusters within Nafton to move toward (away) from the graphene interface, shifting the interface capacitance and affecting the electrical double layer, which consecutively affects the charge carriers' density and graphene channel conductance. To corroborate the hypothesis, we gathered transfer curves of the BLAST devices, shown in Fig. 1e, by fixing drain voltage $V_D = 0.1V$, sweeping gate voltage $V_G$ from 0 V to +2.5 V at varying speeds, and measuring both the drain current ($I_D$, solid curves) and gate current ($I_G$, dashed curves). The measurements show that the charge neutrality point (CNP) of the graphene is ~2 V, which means the graphene is highly p-doped, which is expected considering the graphene was transferred using wet-etch approach. Faster sweeping rate results in increased hysteresis in gate current $I_G$ and a slight leftward shift of the hysteresis, which is expected behavior for ambipolar transistors. The proton accumulation near the graphene interface is shifting the Fermi energy closer to the CNP, resulting in a decreased conductance. We also observe a slight decrease in minimum $I_G$ (see Supplementary Fig. 2), which may be an indication that a limited hydrogen adsorption on graphene is happening. It is also noted that the leakage current is very high in this case. However, this is an artifact of the large area of the device at around 15 mm$^2$. Supplementary Fig. 3 shows a transfer curve of a µBLAST where the gate current is on the order of nA at maximum with a drain current on the order of 100 µA, an expected result for an electrolytic graphene transistor. The leakage current in electrolytic graphene transistors can additionally be explained by the reduction of oxygen in the environment.

Figure 1f shows change in device conductance as a response of cycling pulse trains (positive and negative) for a fixed absolute value current magnitude $I_P$. This is repeated for 5 different current magnitudes, and the result shows that the response is highly reversible and modulated by the strength of the pulse amplitude. To show that the use of graphene is essential in the function of this device, we characterize alternative devices by replacing the active channel layer with another common semiconductor, PEDOT:PSS (see Supplementary Fig. 4). The control devices show no conductance modulation upon current pulses applied through the Nafton gate, because PEDOT:PSS requires bulk electrochemical reactions with mobile protons to modulate the conductance. Since the Nafton is not fully hydrated and there is no proton source at the gate, there are no freely moving protons to deploy. Hence, the observed effect is related to the hybrid interface between graphene and Nafton. We hypothesize that the proton clusters migrate toward the graphene-Nafton interface, forming an electrical double layer and either hole- or electron-doping graphene, a similar mechanism to that seen in supercapacitors with carbon-based electrodes. Our observed surface effect requires far fewer protons to accomplish a conductance change than the bulk electrochemical reaction in PEDOT:PSS due to the atomically thin nature of graphene. Coupled with the slow kinetics of the proton cluster movement within the dry Nafton matrix, long-term potentiation can be explained. It should be noted that voltage pulses can also be used in place of current pulses with the addition of a switch at the gate to open the circuit when a pulse is not being delivered, a common technique to enhance state retention in electrochemical devices. In the case of the BLASTs, current pulses are used due to ease of use in the experimental setup and to promote the linearity and symmetry of synaptic response because the amount of charge delivered to the device mediates the change in conductance. These characteristics will be described in the subsequent section.

High linearity and symmetry in synapse response are essential figures of merit for efficient backpropagation training of neural networks. The conductance evolution behavior of the µBLAST device is linear and symmetric, indicating the potential use in online learning applications. This is evaluated by applying a ramp test: a series of repeated positive and negative spikes cycling the device across its dynamic range. Linearity and symmetry are calculated by collapsing 50 repeated ramping cycles into a single ramp (see Fig. 2a), obtaining the mean and standard deviation conductance of the ramps performed. Non-linearity parameters calculated using previously reported methodology described in Supplementary Note 1 are $\delta_p = 0.89$ and $\delta_n = 0.76$, indicating that performance is approximately linear ($\delta < 1$, where $\delta$ is ideal linearity) and highly symmetric since both directions have the same sign and nearly the same magnitude. As for the number of states achievable, there are 100 explicit conductance states shown in these devices in Fig. 2b. In other experiments, we achieved 300 (see Supplementary Fig. 5) and a maximum of 512 (see Supplementary Fig. 6) specifically defined conductation states, which is more than achieved in other comparable devices. Ultimately, the actual number of states achievable is directly related to the read and write noise levels. The µBLAST devices feature an average read noise calculated (see Supplementary Note 1) to be 0.029% and write noise of around 1.0% (see Fig. 2a, b), corroborating that a high number of effective states can be functionally achieved in the device. The on/off ratio is also high and spans in the range of 200-500, which is comparable to or even exceeds results of competing ionic devices (see Supplementary Table 1). It should be noted that while larger on/off ratios compared to what is shown in Fig. 2a, b can be accomplished by delivering larger write pulses, on/off ratios above 200% are often not desirable in neural network training applications due to the degradation of linearity and symmetry (see Supplementary Fig. 7). However, due to the low read and write noise characterized, the effective number of states should still be high with the caveat that sufficiently high resolution read circuitry can be implemented in the system.

In order to get a complete picture of conductance state control, the relationship between a conductance change ($\Delta G$) per current pulse of different durations and amplitudes is investigated. Mapping of the conductance change as a function of the pulse duration and amplitude (Fig. 2c) shows that $\Delta G$ has an almost linear dependence on the pulse duration and pulse amplitudes. It can be seen (Fig. 2d, e) that $\Delta G$ increases linearly with the increase in either only linear amplitude or pulse duration. Furthermore, there is an evident asymmetry in the response, which becomes more pronounced at higher pulse duration and amplitude. A long positive pulse at high amplitude will result in a much larger magnitude in conductance change than a long negative pulse of high amplitude. However, at lower pulse duration, the $\Delta G$ is approximately the same magnitude for opposite polarity pulses and generally has a linear dependence with pulse amplitude. The change in conductance for 50 ms long pulses deviates from this linear trend, but this is possibly due to the need for a larger magnitude current pulse to overcome intrinsic energy barriers in ion transport within the dry matrix of Nafton.

Finally, we study how channel area affects device performance by building devices with different channel areas, varied from ~10 mm$^2$ to ~100 mm$^2$. For the experiments, both pulse amplitude and duration are kept constant, and a clear decline in the energy normalized conductance change ($\Delta G / G_0$, %/nJ) magnitude is observed (see Fig. 3f) with increasing the device area. Though a linear trend ($R = -0.93$) cannot be concluded due to the appearance of two area-dependent clusters, a general decrease in conductance change as area increases is evident. This is corroborated when only considering devices with channel area larger than 1 mm$^2$ ($R = -0.7$) (see Supplementary Fig. 9). This means that application of the same gate pulses to smaller devices results in
larger effective charge-per-area, resulting in more effective shift in the graphene Fermi level and showing scalability of the BLAST.

To characterize the endurance of a graphene/Na\textsuperscript{+} synapse, long-term pulse cycling (ramp of 20 pulses with 10 µA amplitude and 1 ms duration) is performed for more than ten million cycles (see Fig. 3a). No device performance degradation was seen for up to 10\textsuperscript{7} cycles, which is the maximum capacity of our measurement set-up, and not the limit of mBLAST performance. As one can see from the averaged and collapsed ramp (Fig. 3b), the performance for the first 10\textsuperscript{6} cycles is highly uniform. A more granular representation of the change in ramping characteristics between 10\textsuperscript{6} and 10\textsuperscript{7} cycles is shown in Supplementary Fig. 10. Starting from ~2 × 10\textsuperscript{6} cycles, there is a drop in conductance, which saturates at ~4 × 10\textsuperscript{6} cycles, and is very uniform afterward. Furthermore, when approaching 10\textsuperscript{7} cycles, there is a slight increase in the minimum conductance, along with other changes in the response shape of the ramp. It is important to note that this asymmetry happens only at the lowest conduction points when negative pulses are applied through the gate. This means that median electrostatic charge is gradually shifted, reducing the conductance of the graphene device until the CNP is reached (Dirac point, at approx. +1.8 V, see Fig. 1d). A further change in electrostatic charge will further shift the Fermi level into electron-doping regime, increasing the channel conductance. This feature changes device linearity, but due to the similar magnitude of non-linearity and symmetry, conductance changes performed after 10\textsuperscript{7} pulses would still be effective.

Retention time is another essential figure of merit for synaptic transistors and many neuromorphic computation systems\textsuperscript{47}. In this work, we report on long retention times exceeding 400 seconds (s), shown in Fig. 2b. Another example of this is shown in Fig. 3d, where 50 current pulses are delivered to the device and measurement is continued, allowing the device state to relax. Retention time here refers to the time required for 10% decay of the effective conductance range. Some neuromorphic devices report on much longer retention times\textsuperscript{8,49}; however, when working with biologically relevant systems, the average frequency of events is <1 Hz. Hence, 400 s retention time is adequate. Additionally, due to the dependence of Na\textsuperscript{+} ion conductivity on hydration, there is a possibility to tune the retention by controlling the moisture level in the Na\textsuperscript{+}ion membrane\textsuperscript{50}. The dominance of short-term potentiation depends on the conductance regime of the device, where changes in conductance are primarily short-term when the conductance is near maximum and minimum (see Supplementary Fig. 11). For example, if a positive conductance change is applied when the device is near maximum conductance, the change in conductance will only be retained for several seconds before conductance decays to the value preceding the change. This is an attribute that is common to ionic synaptic transistors of various types\textsuperscript{49,51}. In the timescale of 1 pulse/sec (see Fig. 3e), the device exhibits long-term retention.
plasticity (no conductance decay is present at the scale). As a result, mBLASTs can be operated in variable conductance ranges depending on the balance of needs between retention and dynamic conductance range. It should be noted that the limited retention time of the BLAST devices eliminates the possibility of use in inference-related applications due to the high retention times necessary for those systems. However, in learning-related applications such as a continuously updating biological interface, the retention time shown here is sufficient. The most important figures of merit for neural network training and by extension, continuous learning, are low-energy dissipation per update, favorable synaptic plasticity, and good endurance. Even in the case of adoption in neural network accelerators, though non-trivial, a solution to short retention time can be to use devices that have favorable synaptic characteristics during training (BLASTs), and to then transfer the weights to memory with long retention time for inference when training is finished. As a result, the target application of the BLASTs is for neural network training.

As mentioned previously, for effective online learning, individual write pulses must be energy efficient. Devices of varying area from ~10 mm² to ~100 mm² were fabricated and tested by applying a set current pulse of 1 µA amplitude, 10 ms duration and recording the change in conductance. The calculation of charge modulation through current spike and energy per spike calculation are given in Supplementary Note 2. The energy dissipation per device area is shown in Fig. 4a and is normalized to reflect the energy required to change the conductance of the device by 1% (chosen to approximate a minimum achievable step due to write noise and read noise). The area-normalized energy dissipation per write pulse is very low, far below 1 fJ, the energy dissipation of a biological synapse. It is evident that there is a weak trend of increasing the energy with smaller device area, with µBLASTs exceeding 1 fJ/µm² in energy dissipation, but the results still indicate that device scaling still greatly benefits the devices. These results still exceed or match comparable organic and 2D devices at a competitive speed (see Fig. 4b and Supplementary Table 1).

It is known that Na⁺ ion proton conductivity increases with increased temperature. We conducted experiments with an mBLAST device characterized at temperatures in the range of 0 °C to 80 °C showing marked differences in device performance. As seen in Fig. 3f, the average performance of the synaptic transistor in terms of ΔG improves when temperature is raised from 0 °C to 40 °C (from ~9 µS to ~11 µS), followed by a decrease down to 4 µS at 80 °C. Additionally, while there is no significant change in linearity, there is an increase in write noise up to 22% at 80 °C, shown in Supplementary Fig. 12. We associate the decrease in performance with reduction of Na⁺ hydration due to annealing at temperatures above 40 °C. In bioelectronics-related applications, however, these temperatures should never be reached, and device performance is robust at the relevant temperatures.

The effect of different drain voltage potential V_D on mBLAST performance was also characterized. We found that modulation of V_D has no effect on the maximum and minimum conductance of the synapse (see Supplementary Fig. 14) and does not have a clear effect on either linearity or write noise. As a result, the chosen read voltage does not affect device functionality.

Although the aforementioned mBLASTs are biocompatible, feature superior energy efficiency, and have outstanding neuromorphic...
dissipation is found to be $2.55 \pm 0.39 \text{fJ/} \mu\text{m}^2$. This is most likely due to the usage of a liquid-phase NaF film. Some performance characteristics are notably different compared to mBLASTs, both in the range of over 100 s (see Supplementary Fig. 15). The experimental conductance update characteristics are significantly lower currents required to change the conduction state of the device compared to the larger mBLASTs. The retention time characterized in the µBLASTs is also found to be similar to that of the mBLASTs, both in the range of over 100 s (see Supplementary Fig. 15). Some performance characteristics are notably different compared to the macroscale devices. Firstly, it is important to note that reduction of size yielded an increase in normalized energy dissipation (see Fig. 4a). For devices with channel dimensions $40 \mu\text{m} \times 10 \mu\text{m}$, write energy dissipation is found to be $2.55 \pm 0.39 \text{fJ/} \mu\text{m}^2$ ($N = 4$) for a single update. This is most likely due to the usage of a liquid-phase NaF source material, which is not chemically prepared like thicker NaF films. It is possible that hard-baking the spin-coated NaFon results in less moisture, reducing the density of protonic clusters compared to the preprocessed film. Due to the potential use of microscale devices in an array, read power dissipation needs to be as low as possible to minimize energy dissipation in a crossbar in inference mode. Because of the high conductance of graphene, a low read voltage at 100 mV can be used. A low read power shown in Fig. 5b between approximately 2.5 and 5.0 $\mu\text{W}$ is obtained (see Supplementary Note 3 for calculation). Assuming high frequency read operations are possible (between 1 ns and 100 ns), read energy can easily be sub-pJ. The read energy dissipation can be further improved by optimizing the read voltage to be as small as possible. Figure 5c shows sampled ramp data for four $40 \mu\text{m} \times 10 \mu\text{m}$ devices with conductance and $\Delta G$ ranges within similar ranges of operation. This data is then used to construct the $\Delta G$ vs. $G$ lookup table (LUT) graphs presented in Fig. 5d for the four µBLAST devices. The color-coded plots describe the cumulative distribution function likelihood that a given $\Delta G$ is greater than the expected experimental $\Delta G$. Nonlinearity parameters are also presented for each distribution, and it is evident that there was greater non-linearity for the µBLASTs during positive updates and a relatively linear response for the negative updates, indicating that plasticity is asymmetric. While asymmetric update response is typically considered non-ideal for applications like backpropagation training, we show that such asymmetry of experimental data can yield algorithmic benefits in compute-limited situations.

After analyzing the device characteristics of the mBLASTs and µBLASTs, the experimental conductance update characteristics are used to simulate online learning neuromorphic tasks. The experimental device data is used to construct LUTs that can be directly sampled by the crossbar simulator, allowing the simulation to account for linearity, symmetry, and write noise directly from the experimental results. The following three classification tasks were chosen: (1) Modified National Institute of Standards and Technology (MNIST) handwritten digits recognition, (2) University of California-Irvine Human Activity Recognition (UCI-HAR) dataset for movement classification from biometric sensor data, and (3) Fashion-MNIST clothing article classification. The µBLAST devices were applied on MNIST and UCI-HAR, while the performance of the µBLASTs was evaluated on UCI-HAR and the more complex Fashion-MNIST datasets. Training is accomplished by simulating a small multilayer perceptron with two synaptic weight layers L1 and L2 using CrossSim, a physics-rich neuromorphic crossbar simulator. See Methods for more details on the training simulation setup.

Training performance of the µBLASTs on MNIST as well as the application-relevant UCI-HAR dataset was close to ideal, i.e., matching the test accuracy of a comparison network implemented using numeric weights with 64-bit resolution and ideal backpropagation updates (see Fig. 6a, b), reaching >98% test accuracy on MNIST and >95% test accuracy on UCI-HAR after 20 epochs. This was a direct result of the desirable characteristics of linearity and symmetry quantified previously (see Fig. 2a), along with low write noise.

Due to the unique non-linear and asymmetric update of the µBLASTs, online training performance of a multilayer perceptron on UCI-HAR learned more slowly than ideal synaptic updates, seen in Fig. 6c. However, after 20 epochs, the difference in classification accuracy between the numeric weights and the BLAST synapses was less than 1%, indicating sufficient synapse expressivity to learn a task at the difficulty of UCI-HAR. Training the network on Fashion-MNIST yielded a surprising result (as evident from Fig. 6d): the µBLAST synapse training performance significantly exceeded that of the ideal numeric weights. The improvement in classification accuracy is more pronounced when utilizing the measured synaptic properties of a single device (D1) compared to when the variation across all four devices (D1-4) is accounted for, indicating that D1 has plasticity characteristics, the devices are still rather large. In order to implement more complex neuromorphic functionalities, the device sizes must be scaled down, which we achieved by building microscale devices (µBLASTs). The µBLASTs were made using UV-lithography with HD-8820 passivated graphene field-effect transistors (GFETs, see Fig. 5a). On top of the pre-passivated GFET array, a NaFon-117 containing solution was spin-coated and hard-baked, repeating to obtain three layers of NaFon, with the total thickness of ~650 nm. This high thickness ensures there is no short between the top gate and bottom contacts and thinner NaFon could be used. Similar performance synaptic behavior is observed in the µBLASTs (Fig. 3b), with significantly lower currents required to change the conduction state of the device compared to the larger mBLASTs. The retention time characterized in the µBLASTs is also found to be similar to that of the mBLASTs, both in the range of over 100 s (see Supplementary Fig. 15). Some performance characteristics are notably different compared to the macroscale devices. Firstly, it is important to note that reduction of size yielded an increase in normalized energy dissipation (see Fig. 4a). For devices with channel dimensions $40 \mu\text{m} \times 10 \mu\text{m}$, write energy dissipation is found to be $2.55 \pm 0.39 \text{fJ/} \mu\text{m}^2$ ($N = 4$) for a single update.
characteristics that should be investigated more closely. See Supplementary Fig. 16 for a learning rate sweep confirming this effect. We hypothesize that this improvement in learning is attributed to the unique shape of the synaptic response (see Fig. 5d), where $\Delta G$ is larger at low conductance values and smaller at high conductance values. In other works from others and ourselves, similar update responses, known as metaplasticity, have been shown to be beneficial for online streamed learning$^{63,64}$ and to combat catastrophic forgetting$^{63}$.

To ascertain the functional effect of the metaplastic synapse property, we modified the numeric updates to emulate the LUT of D1. This was done by including a multiplier that depends linearly on the weight value for positive updates while the negative updates were left unchanged. A graphical representation of the update is shown in Supplementary Fig. 17. The resulting test accuracy, shown by the numeric-metaplastic curve in Fig. 6d, closely matches that of experimental LUT$^1$, showing that it is indeed the metaplastic update property of the $\mu$BLAST device that contributes directly to the boost in performance.

To understand how the synaptic metaplasticity affects the high-level properties of the neural network, we examine the final trained weight distributions of two networks: one trained using fully numeric weight updates (without metaplasticity) and one trained using $\mu$BLASTs. The representative distributions for the two neural network layers are plotted in Fig. 6e, f (see Supplementary Fig. 18 for full dataset, including the weight distributions of a numeric metaplastic synapse network). In layer 1, the numeric weights have a remarkably uniform distribution in values, while for $\mu$BLASTs, the weight distribution visibly tapers off away from zero (see Fig. 6e). This effect is more pronounced in layer 2, where there is a prominent peak in weight distribution around zero that is absent from the numeric case. The tendency of the weight distributions to cluster around small absolute values is a natural consequence of the device metaplasticity. The LUTs plot (Fig. 5d) suggests that as the conductance of the device increases, the change in conductance induced by a given pulse is smaller. This has an effect that is equivalent to weight decay regularization$^{65}$, which penalizes large weight values to avoid overfitting to the training set and thus improves the ability to generalize to new examples. This effect is also similar to weight normalization$^{66}$, a technique inspired by batch normalization$^{67}$, both of which are used to train well-regularized neural networks with superior generalizability. The benefit of this regularization was larger for Fashion-MNIST than for the much simpler UCI-HAR classification task, likely because the small multilayer perceptron was relatively under-parameterized for Fashion-MNIST but not for UCI-HAR. Our results indicate that the $\mu$BLAST devices can be used to realize hardware-integrated regularization by taking advantage of metaplasticity. In addition, this result can be extrapolated to other types of devices with similar nonlinear and asymmetric conductance response characteristics where for the same input, there are small conductance changes when updating toward the boundary of the conductance range and large conductance changes when the opposite is true. Two possible candidates that exhibit this behavior can be identified in refs. $^{68,69}$, but are not limited to these examples. The general value of this result motivates a further study of plasticity tuning beyond the established linear and symmetric model.

In conclusion, we have demonstrated a novel solid electrolyte gated graphene device with unique artificial synapse behavior.
experimentally revealed that these bio-compatible devices operate at low energy density (<50 aJ/µm²) at >10 kHz speeds, competitive with other 2D materials-based devices and allowing the potential for the interfacing of biological and artificial synapses. Neural network simulations show that the low read and write noise, coupled with the linear and symmetric synaptic characteristics of the mBLASTs allow for near-ideal classification. More importantly, the µBLASTs are demonstrated to be metaplastic synapses that realize weight normalization, a weight regularization algorithm used to train generalizable neural networks. This allows the performance of µBLAST networks to exceed the classification accuracy achieved by ideal linear numeric weights on difficult tasks. These characteristics make BLAST devices promising candidates in the intersection of bioelectronics and neuromorphic computing.

Methods

Growth of graphene/PMMA stack

The graphene electronic tattoos were fabricated starting with monolayer CVD grown large-scale graphene on copper, purchased from Grolltex. A 2 × 2 in² square was then cut out and spin-coated with PMMA (PMMA 950 A4) to yield a ~200 nm thick layer. To do so, the copper/graphene stack must be placed on a silicon wafer with the graphene facing up. Kapton tape is then used to secure all sides of the copper/graphene stack to the wafer such that a watertight seal is formed under the copper to prevent PMMA from leaking underneath the stack. Afterwards, PMMA (950 A4) is spin-coated onto the stack at ~2500 rpm for 60 s. The sample is then baked on a hotplate at 200 °C for 15–20 min before it is ready for etching.

Graphene/PMMA stack transfer onto tattoo paper

The PMMA/graphene/Cu foil is then placed into ammonium persulfate ((NH₄)₂S₂O₈, 0.1 M) to etch away the copper. The PMMA/graphene film is then cleaned in a series of water washing steps and then transferred onto a temporary tattoo paper. The graphene/PMMA/tattoo paper is then dried and cut into arbitrary desired locations. In order to transfer the graphene/PMMA onto an arbitrary surface, it is first soaked in water for ~5–10 min.

mBLAST device fabrication

The macroscale BLAST devices were fabricated in multiple steps, by combining Nafion 117, PMMA/graphene, conductive adhesive gold tape, and gold/EVA/PET film. The Gold/EVA/PET film is used to form a tight back-gate contact. The fabrication starts by evaporating ~60–90 nm of gold onto an ethylene vinyl acetate (EVA) film. After preparing the gold EVA gate, it is brought in contact with a piece of Nafion strip, adhesive gold contacts are placed 3–10 mm apart from each other, perpendicularly from the gate, on top of the Nafion to form the source and drain terminals. The GETs (~5–15 cm length and 3–10 mm width) are prepared for transfer onto the BLAST device starting by soaking in DI water for 5–10 min. The graphene should show signs of slight separation from the tattoo paper when sufficiently soaked. The GET can then be placed on top of the Nafion and transferred onto the top of the device such that the graphene contacts both gold source-drain contacts and forms a channel across the Nafion.
**µBLAST device fabrication**

CVD grown graphene was covered with a 200 nm thin layer of PMMA for transfer. After etching copper in ammonium persulfate (see above), the graphene was transferred onto the wafer with pre-fabricated Au/Ti (10/50 nm thick) markers. A photoresist was used to protect the graphene channel areas during exposure to oxygen plasma. The stack of 10 nm Ti and 90 nm Au was e-beam assisted evaporated on the wafer through a pre-defined structure of lift-off resists to form source and drain electrical connections. Photostructurable polyimide, HD8820 was used in the last step to form the passivation. Spin-coated at 5000 rpm, exposed at i-line UV light, developed in 0.26% TMAH, and hard baked at 350 °C, the polyimide forms a 3 μm thick passivation. The devices were then diced and spin-coated with the liquid Nafion 117 containing solution (Sigma–Aldrich) three times (3000 rpm, 150 °C bake for 20 mins), forming a 666.7 ± 28.9 μm thick layer.

**Pulse and synaptic measurements**

The three-terminal devices were measured using high-precision source/measure unit Agilent 2902B. One of the SMUs is used to apply 0.1 V of the drain-source potential, while the gate is used in the current-pulsing mode to apply conductance changes.

**Pulse and relax**

Two pulse train tests were used to characterize conductance change due to periodic pulsing. This was done by sending either 50 or 250 consecutive write current pulses with corresponding widths and amplitudes of 100 μs and 100 μA, 1 ms and 10 μA, 10 ms and 1 μA, and 100 ms and 100 nA. All pulse trains were conducted with both positive and negative pulses. The pulses were followed with a 150–200 s relax to observe conductance retention.

**Ramp and level**

A pulse ramp experiment ran multiple sequences of a train of 20 negative pulses followed by a train of 20 positive pulses. The level experiment consisted of an arbitrary sequence of negative and positive current pulses of 10, 20, and 30 μA that were pulsed through the gate every 5 s at a pulse width of 1 ms. Both tests were used to demonstrate distinct and repeatable conductance levels.

**Temperature tests**

The temperature dependence test measured macroscale device performance at varying temperatures (0 °C, 25 °C, 40 °C, 60 °C, and 80 °C). The 0 °C test was performed inside of an insulated Styrofoam container filled with ice. The macro device was lowered onto ice using a petri dish and connected to the Keysight B2902A using wires thin enough as to not disturb the insulating seal. At 25 °C, 40 °C, 60 °C, and 80 °C, the device was secured to the top of a hotplate using Kapton tape while a thermocouple was used to verify the temperature. The above-mentioned tests were performed at each temperature with a minimum time of 30 min after each temperature change to ensure the device was successfully brought to temperature.

**Neuromorphic computing simulations**

Neural network training simulation results and synaptic update lookup tables were generated from experimental data using CrossSim. During a weight update, the ideal backpropagation update is first calculated. To account for synaptic device nonlinearity and write noise, the probabilistic LUT of device updates is queried to sample a conductance change ΔG that depends on the current value of the conductance G of a synapse device. To model device-to-device process variations, each device in the simulated array is randomly assigned to one of four (three) LUTs, each of which is constructed from a different experimentally characterized µBLAST (mBLAST) device. To represent both positive and negative weights, a single weight value is encoded in the difference in conductance between two paired BLAST devices. This is done for two reasons: (1) computing the difference in analog reduces the required dynamic range of the peripheral circuits, (2) using two devices per weight, rather than a fixed analog offset for all devices, avoids coupling the variability and noise in the offset resistor into all the results, which effectively amplifies the variability. When a weight is updated, the conductance of both devices in the pair are updated. The weights are trained using stochastic gradient descent with a batch size of 1, i.e. training samples were shown one at a time. A two-layer MLP was trained for each task, where a sigmoid activation is used after the first layer and a softmax is used after the second layer. The MNIST and Fashion-MNIST networks use a 785 × 300 weight matrix for the first layer and a 301 × 10 weight matrix for the second layer (including bias). The UCI-HAR MLP has a 577 × 200 matrix and a 201 × 6 matrix for the first and second layer, respectively.

**Associated content**

Supplementary Information is available and includes comparison table; Supplementary Notes with calculations of nonlinearity, read and write noise, and energy dissipation; control experiments; additional schematics; detailed datasets and figures.

**Data availability**

The data generated in this study, presented in the Main Text figures, are provided in the Supplementary Information/Source Data. Additional data is available on reasonable request to the corresponding author. Source data are provided with this paper.

**Code availability**

Code available on reasonable request to the corresponding author. CrossSim crossbar simulator available at https://cross-sim.sandia.gov/.

**References**

1. Sebastian, A., le Gallo, M., Khaddam-Aljameh, R. & Eleftheriou, E. Memory devices and applications for in-memory computing. Nat. Nanotechnol. 15, 529–544 (2020).
2. Kim, K.-H. et al. A functional hybrid memristor crossbar-array/CMOS system for data storage and neuromorphic applications. Nano Lett. 12, 389–395 (2012).
3. Burr, G. W. et al. Neuromorphic computing using non-volatile memory. Adv. Phys. X 2, (2017).
4. Bennett, C. H., Garland, D., Jacobs-Gedrim, R. B., Agarwal, S. & Marinella, M. J. Wafer-Scale TaOx Device Variability and Implications for Neuromorphic Computing Applications. in 2019 IEEE International Reliability Physics Symposium (IRPS) 1–4 (IEEE, 2019). https://doi.org/10.1109/IRPS.2019.8720596.
5. Wu, W. et al. A Methodology to Improve Linearity of Analog RRAM for Neuromorphic Computing. in 2018 IEEE Symposium on VLSI Technology 103–104 (IEEE, 2018). https://doi.org/10.1109/VLSIT.2018.8510690.
6. Gallo, M. I. & Sebastian, A. An overview of phase-change memory device physics. J. Phys. D: Appl. Phys. 53, 213002 (2020).
7. Nandakumar, S. R. et al. Experimental demonstration of supervised learning in spiking neural networks with phase-change memory synapses. Sci. Rep. 10, 8080 (2020).
8. van de Burgt, Y. & al. A non-volatile organic electrochemical device as a low-voltage artificial synapse for neuromorphic computing. Nat. Mater. 16, 414–418 (2017).
9. Grollier, J. et al. Neuromorphic spintronics. Nat. Electron. 3, 360–370 (2020).
10. Liu, S. et al. A domain wall-magnetic tunnel junction artificial synapse with notched geometry for accurate and efficient training of deep neural networks. Appl. Phys. Lett. 118, 202405 (2021).
11. Alamdar, M. et al. Domain wall-magnetic tunnel junction spin-orbit torque devices and circuits for in-memory computing. Appl. Phys. Lett. 118, 112401 (2021).
12. Akinola, O. et al. Three-terminal magnetic tunnel junction synapse circuits showing spike-time-dependent plasticity. *J. Phys. D: Appl. Phys.* **52**, 49LT01 (2019).

13. Qin, W., Kang, B. H. & Kim, H. J. Flexible artificial synapses with a biocompatible Maltese–Ascorbic acid electrolyte gate for neuromorphic computing. *ACS Appl. Mater. Interfaces* **13**, 34697–34698 (2021).

14. Kim, Y., Park, C. H., An, J. S., Choi, S.-H. & Kim, T. W. Biocompatible artificial synapses based on a zein active layer obtained from maize for neuromorphic computing. *Sci. Rep.* **11**, 20633 (2021).

15. Hu, L. et al. Ultrasensitive freestanding and mechanically durable artificial synapse with Attojoule power based on Na-Salt Doped Polymer for Biocompatible Neuromorphic Interface. *Adv. Funct. Mater.* **31**, 2106015 (2021).

16. Hussain, T. et al. Cellulose nanocrystal based Bio-Memristor as a green artificial synaptic device for neuromorphic computing applications. *Adv. Mater. Technol.* **7**, 2100744 (2022).

17. Kireev, D. & Offenhäusser, A. Graphene & two-dimensional devices for bioelectronics and neuroprosthetics. *2D Mater.* **5**, 042004 (2018).

18. Oshin, O. et al. Graphene-based biosensor for early detection of iron deficiency. *Sensors* **20**, 3688 (2020).

19. Wang, S., Zhang, D. W. & Zhou, P. Two-dimensional materials for synaptic electronics and neuromorphic systems. *Sci. Bulletin* **64**, 1056–1066 (2019).

20. Wang, C. et al. 2D layered materials for memristive and neuromorphic applications. *Adv. Electronic Mater.* **6**, 1901107 (2020).

21. Chen, S. et al. Wafer-scale integration of two-dimensional materials in high-density memristive crossbar arrays for artificial neural networks. *Nat. Electron.* **3**, 638–645 (2020).

22. Sharbat, M. T. et al. Low-Power, electrochemically tunable graphene synapses for neuromorphic computing. *Adv. Mater.* **30**, 1802553 (2018).

23. Zhu, J. et al. Ion gated synaptic transistors based on 2D van der waals crystals with tunable diffusive dynamics. *Adv. Mater.* **30**, 1800195 (2018).

24. McKnight, R. F. et al. Lithium toxicity profile: a systematic review and meta-analysis. *Lancet* **379**, 721–728 (2012).

25. Han, C. Y. et al. An artificial synapse based on graphene field-effect transistor with silver gel/polarized-aptamer gate. *Org. Electron.* **92**, 106181 (2021).

26. Wei, H. et al. Mimicking efferent nerves using a graphdiyne-based artificial synapse with multiple ion diffusion dynamics. *Nat. Commun.* **12**, 1068 (2021).

27. Schranghamer, T. F., Oberoi, A. & Das, S. Graphene memristive synapses for high precision neuromorphic computing. *Nat. Commun.* **11**, 5474 (2020).

28. Mauritz, K. A. & Moore, R. B. State of understanding of Naion. *Chem. Rev.* **104**, 4535–4586 (2004).

29. Feng, C. & He, P. F. Moisture and thermal expansion properties and mechanism of interaction between ions of a Naion-based membrane electrode assembly. *ASC Adv.* **7**, 34556–34566 (2017).

30. Schmidt-Rohr, K. & Chen, Q. Parallel cylindrical water nanochannels in Naion fuel-cell membranes. *Nat. Mater.* **7**, 75–83 (2008).

31. Kireev, D. et al. Fabrication, characterization and applications of graphene electronic tattoos. *Nat. Protoc.* **16**, 2395–2417 (2021).

32. Kabiri Ameri, S. et al. Graphene electronic tattoo sensors. *ACS Nano* **11**, 7634–7641 (2017).

33. Kim, G. et al. Bacterial adhesion, cell adherence and biocompatibility of Naion films. *J. Biomater. Sci., Polym. Ed.* **20**, 1687–1707 (2009).

34. Turner, R. F. B., Harrison, D. J. & Rojette, R. V. Preliminary in vivo biocompatibility studies on perfluorosulfonic acid polymer membranes for biosensor applications. *Biomaterials* **12**, 361–368 (1991).

35. Guzzo, S. et al. Evaluation of the in vitro biocompatibility of PEDOT:Naion Coatings. *Nanomaterials* **11**, 2022 (2021).

36. Fabbro, A. et al. Graphene-based interfaces do not alter target nerve cells. *ACS Nano* **10**, 615–623 (2016).

37. Park, S. Y. et al. Enhanced differentiation of human neural stem cells into neurons on Graphene. *Adv. Mater.* **23**, H263–H267 (2011).

38. Bendali, A. et al. Vitrofused neurons can survive on peptide-free Graphene Layers. *Adv. Healthc. Mater.* **2**, 929–933 (2013).

39. Pampaloni, N. P. et al. Single-layer graphene modulates neuronal communication and augments membrane ion currents. *Nat. Nanotechnol.* **13**, 755–764 (2018).

40. Wang, H., Wu, Y., Cong, C., Shang, J. & Yu, T. Hysteresis of Electronic Transport in Graphene Transistors. *ACS Nano* **4**, 7221–7228 (2010).

41. Li, S. et al. Large transport gap modulation in graphene via electric-field-controlled reversible hydrogenation. *Nat. Electron.* **4**, 254–260 (2021).

42. Svetlova, A., Kireev, D., Beltramo, G., Mayer, D. & Offenhäusser, A. Origins of leakage currents on electrolyte-gated graphene field-effect transistors. *ACS Appl. Electron. Mater.* **3**, 5355–5364 (2021).

43. Melianas, A. et al. Temperature-resilient solid-state organic artificial synapses for neuromorphic computing. *Sci. Adv.* **6**, 1–7 (2020).

44. Wang, Y. et al. Supercapacitor devices based on graphene materials. *J. Phys. Chem. C.* **113**, 13103–13107 (2009).

45. Li, Y. et al. In situ parallel training of analog neural network using electrochemical random-access memory. *Front. Neurosci.* **15** (2021).

46. Agarwal, S. et al. Resistive memory device requirements for a neural algorithm accelerator. in 2016 International Joint Conference on Neural Networks (IJCNN) 929–938 (IEEE, 2016). https://doi.org/10.1109/IJCNN.2016.7727298.

47. Sun, X. & Yu, S. Impact of non-ideal characteristics of resistive synaptic devices on implementing convolutional neural networks. *IEEE J. Emerg. Sel. Top. Circuits Syst.* **9**, 570–579 (2019).

48. Tian, H. et al. Graphene dynamic synapse with modulated plasticity. *Nano Lett.* **15**, 8013–8019 (2015).

49. Oh, S., Lee, J.-J., Seo, S., Yoo, G. & Park, J.-H. Photodetective artificial synapse and its application to biosignal pattern recognition. *npj 2D Mater. Appl.* **5**, 95 (2021).

50. Schalenbach, M., Lueke, W., Lehner, W. & Stolten, D. The influence of water channel geometry and proton mobility on the conductivity of Naion. *Electrochim. Acta.* **214**, 362–369 (2016).

51. Yang, J.-T. et al. Artificial synapses emulated by an electrolyte-gated Tungsten-Oxide Transistor. *Adv. Mater.* **30**, 1801548 (2018).

52. Huang, H. et al. Electrolyte-Gated Synaptic Transistor with Oxygen Ions. *Adv. Funct. Mater.* **29**, 1902702 (2019).

53. Tsai, H., Ambrogio, S., Narayanan, P., Shelby, R. M. & Burr, G. W. Recent progress in analog memory-based accelerators for deep learning. *J. Phys. D: Appl. Phys.* **51**, 283001 (2018).

54. Zhou, G. et al. Volatile and nonvolatile memristive devices for neuromorphic computing. *Adv. Electronic Mater.* **2101127** (2022). https://doi.org/10.1002/aelm.202101127.

55. Irie, K., Schlag, I., Csordás, R. & Schmidhuber, J. Going Beyond Linear Transformers with Recurrent Fast Weight Programmers. (2021).

56. Kireev, D. et al. Graphene transistors for interfacing with cells: Towards a deeper understanding of liquid gating and sensitivity. *Sci. Rep.* **7**, 1–12 (2017).

57. Siroma, Z. et al. Depression of proton conductivity in recast Naion® film measured on flat substrate. *J. Power Sources* **189**, 994–998 (2009).

58. Li, Deng The MNIST database of handwritten digit images for machine learning research [Best of the Web]. *IEEE Signal Process. Mag.* **29**, 141–142 (2012).

59. Dua, D. & Graff, C. UCI Machine Learning Repository. (2017).
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Author contributions

D.K. and S.L. contributed equally to designing the project, carrying out the measurements, analyzing the data, and writing the paper. H.J. measured the devices and analyzed the data. T.P.X. and C.H.B. carried out the neural network simulations and analyzed the data. D.A. guided the experimental setup, measurements, and direction of the project. J.A.C.I. led the team in the design, measurement, analysis, and writing. The manuscript was written with input from all authors and all authors discussed the results.

Competing interests

The authors declare no competing interests.

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Correspondence and requests for materials should be addressed to Jean Anne C. Incorvia.

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