Glycine gated spiking inhibitory postsynaptic membrane at the synaptic cleft

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ABSTRACT

Background: Enzyme modified field effect transistor (ENFET) may be used to represent the variable conductance of transmitter-gated ion channels in the postsynaptic region of the neuron. Purpose: The objective of this work is to develop a simple analog circuit model that can simulate the function of neurotransmitter glycine gated ion channels of postsynaptic membrane at the synaptic cleft. Methods: In this paper, Glycine sensitive ENFET is incorporated into the Hodgkin-Huxley (H-H) circuit model of the postsynaptic membrane at the synaptic cleft. Results: Simulation of the circuit model yields an output representing the membrane potential of the synaptic region. Simulation is performed in MATLAB environment for inhibitory action of synapses. Conclusion: This model can be used in neuro-bioengineering fields for simulation of binding activity and electrical activity of the postsynaptic region.

KEY WORDS

Neuron Synapse ENFET Postsynaptic membrane Membrane potential Glycine

Introduction

Biologically inspired neuron models are a kind of neuromorphic devices that is an electrical equivalent circuit which is designed to reproduce various phenomena in biological neurons. Biologically inspired neuron models are developed considering electrophysiological behaviour of real neuron. Among the different biologically inspired neuron models, neuron models with enzyme modified field effect transistor (ENFET) are most popular. Studies of biological model involving in vivo and in vitro models for various degenerative diseases such as Age-related macular degeneration (AMD), Alzheimer’s disease (AD), stroke1–6 using wider sample size, involving different parameters could be utilised in simulating the models based on sensor and emitter technology.

2-aminoethanoic acid (Glycine) is an organic compound with the formula NH₂CH₂COOH,7 having a hydrogen substituent as its side chain. Glycine is the smallest of the 20 amino acids commonly found in proteins, responsible for synaptic inhibition in the central nervous system especially in the spinal cord, brainstem and retina.8 Most of the studies, related to iontophoretic application of Glycine in the Central Nervous System(CNS) indicates that it produces inhibitory hyperpolarizing responses in neurons. The hyperpolarizing response occurs due to an increase in the chloride conductance of the neuronal membrane allowing chloride ions to flow down their electrochemical gradient into the cell. The membrane of post synaptic neuron has two types of ion channels-excitatory and inhibitory. The excitatory channels are those which are specific to sodium ions and inhibitory channels are those which are specific to chloride ions. The flow of sodium ions into the cell causes a membrane potential called excitatory postsynaptic membrane potential (EPSP) whereas the flow of chloride ions causes an inhibitory postsynaptic membrane potential (IPSP).

The electrical mechanism of synapse is shown in Figure 1. If the synapse is excitatory, Sodium ions flow into the cell resulting into positive current. As a result the membrane depolarizes. If sufficient number of Sodium channels open, then membrane potential will be greater than the threshold potential Vt of the neuron and initiates an action potential. If the synapse is inhibitory, chloride ions move into the cell, resulting into negative current. As a result the membrane hyperpolarizes. If the numbers of opening of Chloride channels are sufficiently large then membrane potential will be able to initiate an action potential in negative direction. Figure 2 shows the equivalent circuit of a synapse which is developed by adding Hodgkin-Huxley(H-H) equivalent circuit with the presynaptic circuit, where I is the total current from ionic channels of all synapses and E₁, E₂, ... , Eₘ represent the chemical potentials of each corresponding ions. For example, Eₜ may be ENa or may be ECl. The total current I will stimulate the postsynaptic neuron to initiate an action potential.9–12

The total membrane current is divided into two components: a capacitive current and an ionic current. Thus total membrane currents:

Fig. 1: Electrical mechanism of synapse.
where \( V_m \) represents the postsynaptic membrane potential established by the ionic and capacitive membrane current, \( C_m \) is the capacitance of the lipid bilayer of postsynaptic membrane, \( t \) is time.

**Modeling theory of Glycine gated ion channels**

In case of inhibitory action, Glycine is released by the presynaptic terminals into the synaptic cleft. Glycine diffuses through the cleft and bind with specific receptor sites of postsynaptic membrane. In simplest case, the binding reaction may be represented as:\(^{13}\)

\[
\begin{align*}
 & k_1 \\
 & \text{Glycine} + \text{Receptor (closed)} \Rightarrow \text{Glycine} - \text{Receptor (open)} \\
 & k_2
\end{align*}
\]

where \( k_1 \) and \( k_2 \) are the forward and backward rate constants respectively. The field effect transistor (FET) gate surface plays an important role in the sensitivity and stability of the sensor. Each surface layer possesses certain pH sensitivity and can, therefore, detect minute changes in pH close to the electrolyte/insulator interface.

The glycine sensitive ENFET is prepared by immobilizing serine hydroxymethyl transferase on the surface of gate oxide (Ta2O5/Al2O3) (Fig. 3).

\[
\begin{align*}
 & H_3N^+ - CO_2H \leftrightharpoons H_2N^+ - CO_2^- \leftrightharpoons HN^- - CO_2^- \\
 & \text{In aqueous solution glycine itself is amphoteric: at low pH the} \\
 & \text{molecule can be protonated with a pK}_a \text{ of about 9.6 and at} \\
 & \text{high pH it loses a proton with a pK}_a \text{ of about 2.4 (precise values} \\
 & \text{of pK}_a \text{ depend on temperature and ionic strength). The nature} \\
 & \text{of glycine in aqueous solution has been investigated by theoretical} \\
 & \text{methods.}^{14} \text{In solution the ratio of concentrations of the} \\
 & \text{two isomers is independent of both the analytical concentration} \\
 & \text{and of pH. This ratio is simply the equilibrium constant for} \\
 & \text{isomerization. Glycine is not essential to the human diet, as it is} \\
 & \text{biosynthesized in the body from the amino acid serine, which} \\
 & \text{is in turn derived from 3-phosphoglycerate. In most organisms,} \\
 & \text{the enzyme Serine hydroxymethyl transferase catalyses this} \\
 & \text{transformation via the cofactor pyridoxal phosphate:}^{15} \\
 & \begin{align*}
 & \text{serine + tetrahydrofolate} \rightarrow \text{glycine} + N^5, N^{10}-\text{Methylene tetrahydrofolate} + H_2O \\
 & \text{NH}_3 \text{-CH}_2\text{COO}^- \text{+ THFA} \rightarrow \text{NH}_3\text{-CH}_2\text{COO}^- + N^5, N^{10}-
\end{align*} \\
 & \text{Methylene THFA} + H_2O
\end{align*}
\]

The proton generated in this reaction changes the pH inside the enzyme which is registered by the underlying ion sensitive FET. The threshold voltage of such device, \( V_{th(IS)} \), is a function of pH solution dependent on the concentration of glycine. For very small value of drain to source voltage of ENFET, \( V_{ds} \), the conductance of such ENFET can be expressed as:\(^{16}\)

\[
G_{ds} = \beta (V_{gs} - V_{th(IS)})
\]  

\( \beta \) is the geometric sensitivity parameter given by

\[
\beta = \mu C_o (W/L)
\]

where \( C_o \) is the oxide capacity per unit area, \( W \) and \( L \) are the width and the length of the channel respectively, and \( \mu \) is the
electron mobility in the channel. \( V_m \) is the voltage applied to the reference electrode and \( V_{th}(IS) \) is the threshold voltage of the ENFET. In ENFET, \( \beta \) and \( V_{th}(IS) \) are constants and \( V_{th}(IS) \) is the only input variable. Thus \( G_m \) is dependent on the threshold voltage, \( V_{th}(IS) \), analogous to the conductance of ion channels of postsynaptic membrane dependent on the binding activity. The neurotransmitter gated ion channels can therefore be represented by glycine sensitive ENFET due to its variable nature of conductance with respect to voltage. Glycine receptor binding activity is a time dependent phenomenon and therefore number of opening of transmitter gated ion channels will be varying with respect to time. \( V_{th}(IS) \) in equation (2) can, therefore, be modeled as:17

\[
V_{th}(IS)(t) = V_{th0}[1 - \exp(-k_1 t) + \exp(-k_2 t)U(t - t_m)] \tag{3}
\]

where \( k_1 \) and \( k_2 \) are time constants analogous to the rate constants of equation (1), \( U(t-t_m) \) is the Heaviside function and \( V_{th0} \) is the threshold voltage proportional to the maximum attainable conductance, when all the transmitter-gated channels for Cl ions are open.

Modeling neuron for inhibitory synapse

The modeling for inhibitory synapse is shown in Figure 4. Considering only Cl-channels to be responsible for inhibitory action, the post synaptic membrane is divided into three patches to represent spatial summation of the Chloride current controlled by

\[
I_n = I_1 + I_2 + I_3 \\
I = C(dV_m/dt) + g_{Cl}(V_m - E_{Cl}) + g_K(V_m - E_K)
\]

where \( g_{Cl} \) is the total Chlorine conductance and \( g_K \) is the nongated potassium conductance. \( V_{Cl}, V_{g1}, \) and \( V_{g2} \) are the voltages applied to the reference electrodes of the ENFETs. The membrane potential \( V_m \) is obtained by spatially and temporally varying \( g_{Cl} \) of Glycine-gated Chlorine channels.

A spiking model is a mathematical model which describes how input spike trains (sequences of timings) are mapped to an output spike train. Thus the output can be characterized by

\[
S = (t_i; i = 1, 2, \ldots, n), t_i < t_{i+1}
\]

Where \( t_i \) is the \( i^{th} \) spike train in a train of \( n \) spikes.18 The spiking strategy that is used in Glycine gated postsynaptic membrane is by integrating the differential equation for membrane potential with Euler approximation method and then thresholding the output.

Simulation

The component values assigned in the model for MATLAB simulation are19: \( C_m = 1 \mu F \) per cm\(^2\), \( g_K = 1 \) mS per cm\(^2\), \( E_{Cl} = -100 \) mV and \( E_K = -90 \) mV. The specifications for three p-channel MOSFETs are \( L = 15 \mu m, W = 2 \mu m, t_{ox} = 100 \) nm, \( \mu = 600 \) cm/\( V \)-sec. The parameters for exponential function in equation (3), applied to each MOSFET inputs are: \( V_{th} = -5 \) Volts, \( t_m = 850 \) \mu sec, \( K_1 = K_2 = 0.8 \) msec.

Results

The MATLAB simulation outputs are shown below (Fig. 5). The waveform represents the normal postsynaptic membrane potential with respect to time. \( V_m \) is established by spatial summation and temporal integration of the glycine-gated current. In this model, action potential is inhibited whenever the membrane potential is depolarized to a value of 65 mV and after that the action potential is reset to a value of -35 mV; The action potential thus takes the form of spikes and occurs during the time period of the pulse.

Conclusions

Thus glycine-sensitive ENFET can be used as circuit analog to simulate the inhibitory postsynaptic membrane potential. Both in neurology and bioelectronics area this biologically motivated model may become a useful tool for research and teaching unit. This approach of the model can be used for various other types of neurotransmitter-gated channels to reproduce a wide variety of electrical responses.
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