Cardiovascular MRI in clinical trials: expanded applications through novel surrogate endpoints

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ABSTRACT
Recent advances in cardiovascular magnetic resonance (CMR) now allow the accurate and reproducible measurement of many aspects of cardiac and vascular structure and function, with prognostic data emerging for several key imaging biomarkers. These biomarkers are increasingly used in the evaluation of new drugs, devices and lifestyle modifications for the prevention and treatment of cardiovascular disease. This review outlines a conceptual framework for the application of imaging biomarkers to clinical trials, highlights several important CMR techniques which are in use in randomised studies, and reviews certain aspects of trial design, conduct and interpretation in relation to the use of CMR.

INTRODUCTION
The randomised controlled trial (RCT) is the gold standard approach to the evaluation of a new proposed therapy for cardiovascular disease.1 2 The growth in the number and scale of RCTs is in part a consequence of the growth in candidate drug targets, driven by new technologies for drug discovery and screening and by a need to test targets, driven by new technologies for drug discovery and screening and by a need to test targets. Despite a theoretically favourable direction of movement of circulating biomarkers. CMR and cardiovascular magnetic resonance (CMR) offers a range of powerful imaging3 and spectroscopic4 techniques which can be used to identify suitable participants for entry into trials, to ensure baseline comparability of treatment arms and to generate markers of disease presence, severity or activity for use as outcome measures in clinical trials. Many of these CMR-derived markers have been validated,5−14 and increasingly have been shown to be closely linked to important clinical endpoints.15 These developments have led to a rapid increase in their use in clinical trials, a trend which is likely to continue. The versatility of CMR arises from the wide range of sequences available, but only a limited number can reasonably be applied to one individual during a CMR study lasting perhaps 60 min. Each technique differs in terms of its accuracy, precision, reproducibility, sensitivity, link with clinical endpoints and ease of use in terms of both acquisition and analysis. Trialists must therefore understand these characteristics for each outcome measure selected.

The development and evaluation of a potential new therapy is a complex process which varies substantially in terms of time, costs and difficulty, depending on the target condition and the therapy proposed. CMR may have a role in several of the four phases of drug or device development: to identify suitable participants for enrolment and to confirm baseline distribution of key prognostic factors in different treatment arms at any phase of treatment evaluation; to establish efficacy in phase II and III studies, where it may be used to inform a large-scale RCT of ‘hard’ clinical outcomes; to extend the application of a proven therapy to other groups of patients.

Reconciling the expanding pool of candidate therapies and indications for treatment with the desire to have the best possible evidence for efficacy, safety and clinical effectiveness represents a significant challenge.16 One approach is to accept only hard clinical outcome-driven studies, accepting that the resources required to do this mean that only a small number of particularly promising therapies will be evaluated. In this model, CMR may have an important role in identifying the most promising therapies for further evaluation. A second approach is to broaden the scope of therapies but to evaluate them in restricted patient groups, commonly high-risk groups (who are most likely to experience clinical events). Here, CMR may have a role in confirming efficacy in wider patient groups. A third approach has been to measure a circulating biomarker which is linked to disease severity and to assume that, if the biomarker moves in a direction thought to be advantageous, this will correspond to a consequent reduction in clinically meaningful endpoints.17 While such studies may be useful in demonstrating efficacy, recent high-profile studies highlight the risks inherent in assuming that a single circulating biomarker can adequately capture all of the relevant consequences of manipulating a complex biological system.18 For example, in the ILLUNATE study,19 the CETP inhibitor torcetrapib was shown to worsen clinical outcome despite a theoretically favourable direction of movement of circulating biomarkers. CMR and other imaging modalities may have an intermediate role between early studies showing potential benefit in single biomarkers and large-scale RCTs using clinical outcomes. It is of interest that two imaging studies of torcetrapib (RADIANCE19 and ILLUSTRATE20) did not demonstrate plaques.

The advantage of imaging surrogate endpoints over circulating surrogate biomarkers is that they capture the downstream activation or final pathway of disease progression, whereas circulating biomarkers may interrogate a single pathway which may be only one of many relevant pathways. Imaging surrogate endpoint studies can have an important (though not exclusive) role in the evaluation of potential therapies taking place after animal and human dose-ranging studies (phase I−II) but before (and generally as a supplement to or screening process for) large-scale randomised trials. In such cases, it may be that
CMR can reliably discriminate clinically important treatment differences with smaller sample sizes than less precise biomarkers, and hence provide results more rapidly and at a potentially lower overall cost than other surrogate endpoints. In all cases, good pharmacovigilance practice will continue to be of great importance.22

DEFINITION OF TERMS
The Biomarkers Definitions Working Group of the US National Institutes of Health defines a biomarker as a characteristic that is objectively measured and evaluated as an indicator of normal biological processes, pathological processes or pharmacological responses to a therapeutic intervention.23 Surrogate endpoints are those biomarkers which are intended to substitute for clinical endpoints in clinical research studies and, as such, are expected to predict clinical benefit (or harm) based on epidemiological, therapeutic, pathophysiological or other scientific evidence. The distinction between biomarker and surrogate endpoints is important, emphasising that only a proportion of biomarkers can be regarded as surrogate endpoints—namely, those that can predict clinical outcomes. The Working Group definition draws a distinction between biomarker (or surrogate endpoint) for efficacy and biomarker (or surrogate endpoint) for toxicity, usually safety. Imaging endpoints such as those acquired using CMR are predominantly endpoints for efficacy, and there has been a concerted effort within the field in recent years to link imaging biomarkers to clinical outcomes, and these will be augmented by ongoing and future large-scale longitudinal studies.

SURROGATE ENDPOINTS
The essential feature of a surrogate endpoint is its sensitivity. Clinical events are generally insensitive markers of disease activity because clinical events are generally rare and so typically require large numbers of individuals to be followed for protracted periods. Surrogate endpoints are more sensitive markers of disease presence, severity or activity, are usually continuous variables, and so are ‘common’ and therefore reduce the sample sizes required to have a certain power to detect an effect of given clinical and statistical significance. These reductions in sample size can often be translated into reduced cost and duration of a trial compared with a study based on clinical endpoints or trials using less precise surrogates. The use of surrogate endpoints of all types has come under close scrutiny in recent years. Historically, the CAST trials (in which encainide and encainide reduced arrhythmias after myocardial infarction but increased mortality) were among the first to highlight the possibility of discordance between the direction of movement of a surrogate endpoint and clinical outcome.24 More recently, the ILLUMINATE study19 showed no net benefit of treatment (indeed, as noted above, it showed potential for harm), yet the biomarker changes would have anticipated benefit. A limitation of all surrogate endpoint studies is that even the best marker of disease presence and activity provides only limited (if any) information about the effects of the drug in question on organ systems or processes which are not the target pathophysiological process. These so-called off-target effects, such as liver dysfunction or QT interval prolongation, are important and need to be rigorously evaluated prior to the universal uptake of such therapies (box 1).

CMR: A RANGE OF TECHNIQUES WHICH CAN GENERATE IMAGING SURROGATE ENDPOINTS
In general, CMR as a technique has several strengths which make it, for many applications, the imaging modality of choice for assessing the cardiovascular phenotype. First, it provides inter alia a versatile and sensitive assessment of many aspects of cardiovascular structure and function; these include ventricular function, valve function, vascular anatomy and function, determining the presence and extent of myocardial scar, evaluating myocardial perfusion and myocardial tissue characteristics. Second, it is safe, well-tolerated, non-invasive and, because no ionising radiation is used (unlike CT and nuclear methods), it lends itself to studies making repeated measures of the same individual—for example, before-and-after treatment phases—with potentially important reductions in sample size (and hence cost) for a given power, statistical significance threshold and predicted treatment effect size. Third, CMR allows assessment of parameters that cannot easily be evaluated in any other way and therefore provides a unique insight into some aspects of cardiovascular disease processes—for example, T2 imaging for myocardial oedema30 and T2* imaging for the assessment of myocardial iron overload.11 31 Fourth, there is now a robust evidence base for the validation and reproducibility of many CMR techniques and an emerging pool of data regarding the prognostic implications of CMR surrogate endpoints.15

LIMITATIONS OF CMR FOR CLINICAL TRIALS
Several limitations must be considered when planning CMR clinical trials. Implanted pacemakers, defibrillators and resynchronisation devices generally preclude CMR imaging on safety grounds, although strategies to reduce risk can be employed in the clinical arena.32 This is an important limitation, particularly for studies of patients with advanced cardiac disease in whom treatment effects are perhaps easier to detect and for whom new treatments are most likely to be of benefit. Another barrier to CMR use in clinical trials is logistics. CMR systems require major investment in hardware, software, infrastructure and maintenance, and access is limited in many parts of the world. The technique is complex and substantial training and experience is required to allow accurate measurements. There may be limited transferability of some sequences across vendors, field strengths and different sites using the same system and field strength. Standardised protocols for data acquisition and analysis, often with core-lab data analysis, are essential in the clinical trial setting and these have been and are being developed by the Society for CMR, along with a registry of clinical trials involving CMR.53

CMR mandates a period of relative inaccessibility of the participant while scans are acquired and so cannot be performed at certain times in a patient’s clinical care; this can limit its usefulness in some types of study. An important example is patients with ST elevation myocardial infarction (STEMI) undergoing primary percutaneous coronary intervention (PCI)
in whom it is clearly not feasible to perform CMR in the immediate phase of admission prior to urgent reperfusion therapy. This limits the use of before-and-after study designs for the evaluation of new therapeutic adjuncts to primary angioplasty in STEMI. It should be noted, however, that safe imaging of patients with recent myocardial infarction is highly feasible in experienced units with careful safety planning and robust plans for patient evacuation and resuscitation, and has been used in a number of studies.

Optimal time point selection is an important aspect of the application of CMR to clinical trials. Several CMR surrogate endpoints of disease visualise and quantify a highly dynamic process, such as the evolving extent of markers of myocardial reversible and irreversible damage as scar and ventricle remodel in the weeks following a myocardial infarction. This inherent within-patient variability means that time point selection is critical.

The strengths and weaknesses of CMR for clinical trials are shown in box 2.

**SELECTION CMR TECHNIQUES USED FOR CLINICAL TRIALS**

A wide variety of CMR sequences, protocols and analysis techniques are available to the trialist. Some of these approaches generate surrogate markers which are widely accepted and some, while validated, remain experimental in a clinical trial context because the prognostic implications of the biomarker are uncertain. The selection of a surrogate marker depends upon the question under study and the way in which a trial will be interpreted. We highlight here just three examples of categories of parameters which can be measured and discuss the extent to which they meet the criteria listed above for a good surrogate marker. We also discuss limitations and give some examples of their use in recent randomised trials.

**VASCULAR IMAGING**

Atherosclerosis is the leading cause of death in developed countries, and emerging therapies will continue to focus on disrupting the pathways which lead to the progression and destabilisation of atherosclerotic plaque. CMR has recently been used in a number of RCTs, and a role complementary to other imaging modalities is emerging for clinical trials in atherosclerosis. Quantitative coronary angiography, intravascular ultrasound, optical coherence tomography, carotid-intima media thickness, CT and positron emission tomography all have advantages in different settings, but the strength of CMR lies in its ability to discern distinct plaque components non-invasively, repeatably and with small sample sizes.

Atherosclerosis imaging by CMR can measure a number of aspects of large artery (aorta and carotid) arterial wall structure and function. The non-invasive nature of CMR allows serial imaging of the same region of vasculature and the same plaque over time without ionising radiation, although gadolinium-based contrast agents are sometimes needed. Several measures have now been standardised and can be routinely measured by experienced core-labs: wall area and wall volume both measure plaque volume whereas minimal lumen area and plaque eccentricity measure degree of intrusion of the plaque into the lumen and disposition of the plaque, respectively. These measures are highly reproducible and agree closely with histological and ex vivo magnetic resonance measures.

Saam et al have provided reproducibility calculations for several CMR atherosclerosis measures based on serial magnetic resonance data from the placebo group of an RCT. Corti et al used CMR to demonstrate reductions in wall area and wall thickness in both the carotid and thoracic aorta over 24 months in an RCT of simvastatin in 18 individuals with known atherosclerotic plaque. Lee et al showed a decrease in carotid wall area with modified-release nicotinic acid in 17 statin-treated patients over 12 months, several years before large-scale clinical endpoint studies are scheduled to report.

A recent change of emphasis in atherosclerosis imaging is from measures of plaque extent to attempts to evaluate the biological activity or risk posed by a plaque, using techniques which measure plaque composition or biological activity including inflammation or markers of vascular elastic function. CMR can assess the fibrous cap, the lipid-rich/necrotic core, the presence, extent and age of intra-plaque haemorrhage and the relative contribution of loose and dense fibrous tissue to the plaque. AHA lesion classification, soft plaque identification and plaque risk assessment may be achieved. The ORION study showed regression of the lipid-rich necrotic core of carotid plaque using rosvastatin over 2 years, demonstrating that serial carotid magnetic resonance could evaluate regression of individual plaque components, with particular significance for a number of emerging proposed therapies for atherosclerosis.

Current research efforts in CMR atherosclerosis imaging are investigating putative markers of the biological activity of the plaque, particularly with respect to inflammation. Ultra-small superparamagnetic iron oxide (USPIO) particles injected intravenously may reflect macrophage activity, and the recent Atheroma trial showed a reduction in USPIO accumulation in carotid plaque in subjects randomised to high-dose compared with low-dose atorvastatin. CMR can evaluate the functional consequences of atheroma burden on the elastic function of arteries and can measure both regional and global aortic stiffness. Furthermore, the forces and shear stress acting on the wall of the artery can now be measured. Low wall shear stress and high oscillatory shear index have been linked to endothelial activation.

At present, high resolution CMR arterial wall imaging and plaque characterisation is available only for large, relatively immobile arteries, and the walls of the coronary arteries in particular cannot be assessed in this way owing to their small size, mobility and tortuosity. While carotid and abdominal aortic atheroma are of clinical relevance and probably broadly reflect the overall atheroma burden, extrapolation of atheroma
Box 3 Atherosclerosis imaging by cardiovascular magnetic resonance

- Plaque anatomy
  - Wall area
  - Wall volume
- Plaque lumen effects
  - Minimal lumen area
  - Plaque eccentricity
- Wall composition
  - Fibrous cap classification
  - Lipid-rich/necrotic core
  - Intra-plaque haemorrhage
  - Dense/loose fibrous tissue
- Wall mechanics
  - Compliance
  - Distensibility
  - Wall shear stress
  - Oscillatory shear index
- Biological activity
  - Inflammation

regression at one site to other vascular beds may not always be
justified. In a study by Yonemura et al the reduction in plaque
volume seen in the carotid artery with high-dose atorvastatin
was not seen in the abdominal aorta.46

There is correlation between Framingham risk and CMR
markers of atherosclerosis,47 and small studies have suggested
that carotid CMR findings predict the subsequent risk of
stroke,48 49 but the predictive value of such imaging beyond
standard risk prediction scores has not yet been proven in large
longitudinal studies, although such studies are underway (box 3).

INFARCT SIZE BY LATE GADOLINIUM ENHANCEMENT (LGE)
The development of new therapies for the treatment of ongoing
or completed myocardial infarction is an important goal in
cardiovascular drug and device development. The improvements
in mortality and morbidity following myocardial infarction in
recent years mean that demonstrating a further reduction
requires large sample sizes. A number of CMR techniques are
now well established in the clinical evaluation of patients with
acute and chronic myocardial infarction and have been reviewed
recently.50–52 CMR affords a highly accurate means of quantifying
the size6 of myocardial infarction (figure 1) and this, combined with
accurate measures of left ventricular volumes, systolic function,
wall thickness and wall thickening, allows the accurate charac-
terisation of the ‘severity’ of myocardial infarction with much
greater sensitivity than clinical endpoints (even when these are
combined as composite endpoints). Infarct size is a powerful
predictor of subsequent clinical outcome53 and recent studies
have reported that infarct size measured by LGE-CMR is a
stronger predictor of clinical outcome than left ventricular
ejection fraction or left ventricular volumes.54–56 LGE-CMR may have advantages over nuclear techniques for the evaluation
of new therapies in some contexts. Specifically, the increased
sensitivity of CMR for subendocardial infarction of <50%
transmural extent in both acute57 and chronic infarction58 is
likely to reduce sample sizes. Kim et al have recently reviewed
the role of CMR in both the clinical management and in infarct
size measurement in clinical trials of myocardial infarction59 and
make several important points relevant to the use of this tech-
nique. First, infarct size evolves over the days and weeks following a myocardial infarction so imaging studies are most
likely to be useful after 3 months post-infarct. Second, trans-
parency in reporting the time after the infarct is essential. Third,
serial imaging of infarct size is not feasible in many trials of
acute myocardial infarction because of the clinical condition of
the patient on arrival in hospital and the need for emergency
care; thus the advantage of high reproducibility of the technique
may be offset by the inability to acquire before-and-after treat-
ment imaging data. As a result, paired tests (before/after) may
not be possible and the large reductions in sample size seen in
some other contexts60 61 may not be realised. While this is true
for the evaluation of therapeutic interventions that need to be
instituted within minutes to hours (such as potential improve-
ments of primary PCI), it may be possible to achieve sequential
imaging where the treatment is to be administered subacutely
(eg, several hours to several days after admission) or with elective
procedures (eg, coronary artery bypass graft or complex PCI).60 61 Importantly, LGE used in a parallel (rather than
repeated measures) study design still requires only a fraction of
the sample size compared with other less reproducible tech-
niques. CMR methods were used to evaluate adjuncts to
primary PCI in the CE-MRI sub-study of the EXPIRA study,
showing reduced infarct size by LGE-CMR in patients ran-
domised to receive adjunctive thrombectomy using a manual
device during primary PCI for STEMI.62

VENTRICULAR VOLUMES, MASS AND FUNCTION
The ability of CMR to measure ventricular volumes, mass and
function accurately, reproducibly and on serial studies without

Figure 1 Late gadolinium quantification. Inversion-recovery short
axis image of the left ventricle after administration of a gadolinium-based
contrast agent showing (A) endocardial and epicardial contours, definition of
a region of remote myocardium, and (B) automated segmentation of infarcted
from non-infarcted myocardium (based on >2SD pixel intensity compared with
remote myocardium).
significant risk to the patient is a major strength of CMR for clinical trials. Bellenger et al demonstrated substantial sample size reductions (of 81–97%) if CMR measures of volumes, mass and function were serially obtained compared with echocardiography. The sample sizes required for left ventricular mass in particular were small (n=9 for each group to detect a 10 g change in left ventricular mass with a power of 90% and p value of <0.05), based on the high reproducibility of this measure by CMR. This is of relevance to conditions in which ventricular performance or responses are important such as hypertension. Several recent studies have evaluated emerging therapies for hypertension using left ventricular mass index as a primary endpoint. The ALLAY study used a non-inferiority study design to show that the direct renin inhibitor aliskiren was non-inferior to losartan monotherapy in reducing left ventricular mass index. The effect of the phosphate binding drug sevelamer is currently being evaluated to determine its effects on left ventricular mass in patients with early kidney disease, demonstrating that the current use of CMR endpoint studies is not confined to therapies conventionally regarded as being primarily used for cardiovascular indications. CMR may also have a role as part of broader cardiovascular safety studies for drugs intended to treat both cardiovascular and non-cardiovascular conditions.

CURRENT USE OF CMR IN CLINICAL TRIALS
The number of clinical trials using CMR has grown rapidly in recent years. We searched the NIH international trials register for completed registered clinical intervention trials with at least one endpoint including CMR using the search terms (cardiac OR vascular OR cardiovascular) AND magnetic AND resonance. We excluded studies which were principally intended to evaluate diagnostic performance of an imaging modality. Fifty-five studies fitted these criteria with total enrolment of 5659 subjects. The mean (SD) sample size was 105 (95) enrolled subjects; 24 studies evaluated treatments for myocardial infarction and nine studies evaluated atherosclerosis. A CMR endpoint was the primary endpoint in 44 of the 55 studies and, in these studies, well-established endpoints such as left ventricular volumes, mass or function were used more frequently (23 studies) than less well-established biomarkers such as USPIO-enhanced MRI signal in carotid plaques (1 study). Unregistered trials and studies registered on other databases were not captured, so these figures probably represent an underestimate of the use of CMR internationally for this type of study.

CLINICAL TRIAL PRINCIPLES FOR CMR
The increasing use of CMR for the clinical evaluation of new therapies will require close collaboration between CMR practitioners, pharmacologists, trialists, statisticians and the pharmaceutical industry. Good practice regarding clinical trial design, conduct, analysis and reporting is essential in CMR trials, and training in these areas will be required for CMR practitioners who are involved with clinical trials.

TRIAL DESIGN
CMR is well suited to a number of study designs (figure 2). Crossover studies, in which each participant is randomly allocated to a sequence of therapeutic arms, are particularly to be

Figure 2 Four different study designs. Upper panels show crossover designs, lower panels show parallel designs. Panels on the left show single cardiovascular magnetic resonance (CMR) scan per treatment phase, panels on the right show before/after scans for each treatment phase.
encouraged where the therapy in question is likely to have fairly rapidly reversed effects on a long-term condition, in view of the favourable effects of this design on sample size, for a given power and level of statistical and clinical significance (figure 3).

TRIAL ANALYSIS
CMR sequences, protocols and endpoints should be prespecified in the trial protocol, which should be registered and published.66 One endpoint should be specified as the primary endpoint. CMR outcome assessment can often (but not always) be blinded to treatment allocation. Artefacts related to treatment allocation will sometimes compromise blinding of outcome assessment—for example, artefacts related to sternal wires in trials of coronary artery bypass grafting versus medical therapy.67

Figure 3  Effect of study design on sample size, assuming a given level of power and statistical significance, to discriminate a clinically important difference for four cardiovascular magnetic resonance surrogate markers. EF, ejection fraction; LV, left ventricle; P(WV), pulse wave velocity; RV, right ventricle.

TRIAL REPORTING
Clinical trials using CMR to evaluate an investigational medicinal product or other intervention should be reported and considered for publication if they address an important clinical question, with robust methods and are adequately powered, regardless of the direction or magnitude of the study findings.68 CMR trials should adhere to CONSORT guidelines for clinical trial reporting,69 and reports should pay particular attention to the method of randomisation, allocation concealment and blinding and should make clear which analyses and endpoints were prespecified (and therefore hypothesis-testing) and which were not (and therefore hypothesis-generating).

CONCLUSION
More than ever, the process of identifying promising therapies and their evaluation from the laboratory to the clinic requires collaboration between widely differing fields. The versatility and power of CMR to address key issues in the evaluation of therapies for many cardiovascular diseases means that close collaboration will be needed between CMR specialists and others involved in clinical trials. This will ensure best use of the opportunity which CMR affords to evaluate promising new therapies and ultimately to deliver these therapies to patients with cardiovascular disease.

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Competing interests PE is a member of the UK Biobank Steering Committee and Chair of the UK Biobank Enhancements subgroup which is considering addition of CMR measurements in a subsample of UK Biobank participants. AP and SEP are involved in the design and conduct of clinical trials using CMR to evaluate new therapies, some of which involve some funding from the pharmaceutical industry.

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REFERENCES
1. Yusuf S, Collins R, Petro R. Why do we need some large, simple randomized trials? Stat Med 1984;3:409–22.
2. Ioannidis JP, Haidich AB, Pappas M, et al. Comparison of evidence of treatment effects in randomized and nonrandomized studies. JAMA 2001;286:821–30.
3. Penrell DJ. Cardiovascular magnetic resonance. Circulation 2010;121:992–705.
4. Hudsmith LE, Neubauer S. Magnetic resonance spectroscopy in myocardial disease. JACC Cardiovasc Imaging 2009;2:87–96.
5. Kim RJ, Fiore D, Penent T, et al. Relationship of MRI delayed contrast enhancement to irreversible injury, infarct age, and contractile function. Circulation 1999;100:1992–2002.
6. Kim RJ, Wu E, Rafael A, et al. Use of contrast-enhanced magnetic resonance imaging to identify reversible myocardial dysfunction. N Engl J Med 2000;343:1445–53.
7. Cheng AS, Pegg TJ, Karamitos TD, et al. Cardiovascular magnetic resonance perfusion imaging at 3 Tesla for the detection of coronary artery disease: a comparison with 1.5 Tesla. J Am Coll Cardiol 2007;49:2440–9.
8. Leeson CP, Robinson M, Francis JM, et al. Cardiovascular magnetic resonance imaging for non-invasive assessment of vascular function: validation against ultrasound. J Cardiovasc Magn Reson 2006;8:381–7.
9. Grootenhuis HB, Westenberg JG, Steendijk P, et al. Validation and reproducibility of aortic pulse wave velocity as assessed with velocity-encoded MRI. J Magn Reson Imaging 2009;30:521–7.
10. Cawley TP, Maki JH, Otto CM. Cardiovascular magnetic resonance imaging for valvular heart disease: technique and validation. Circulation 2009;119:488–78.
11. Anderson LJ, Holden S, Davis B, et al. Cardiovascular T2-star (T2*) magnetic resonance for the early diagnosis of myocardial iron overload. Eur Heart J 2010;31:2171–9.
12. Lockie T, Ishida M, Perera D, et al. High-resolution magnetic resonance myocardial perfusion imaging at 3.0-Tesla to detect hemodynamically significant coronary stenoses as determined by fractional flow reserve. J Am Coll Cardiol 2010;57:90–9.
13. McComnis KS, Goldstein TA, Abendshien DR, et al. Quantification of regional myocardial oxygenation by magnetic resonance imaging: validation with positron emission tomography. Circ Cardiovasc Imaging 2010;3:41–6.
14. Keenan NG, Sheppard MN, Grasso A, et al. Validation of carotid arterial wall volume measurement by cardiovascular magnetic resonance. J Magn Reson Imaging 2010;31:935–41.
15. Hombach V, Merkle N, Bernhard P, et al. Prognostic significance of cardiac magnetic resonance imaging: update 2010. Circ Cardiovasc Imaging 2010;3:1549–57.
16. Sang NS, Crowley WF Jr, Genel M, et al. Central challenges facing the national clinical research enterprise. JAMA 2005;293:1278–79.
17. Lonn E. The use of surrogate endpoints in clinical trials: focus on clinical trials in cardiovascular diseases. Pharmacoepidemiol Drug Saf 2001;10:497–508.
18. Pfeffer MA. ACCORDing to a trialist. Circulation 2010;122:841–3.
19. Barter PJ, Caulfield M, Eriksson M, et al. Effect of torcetrapib in patients at high risk for coronary events. N Engl J Med 2007;357:2109–22.
20. Nissen SE, Tardif JC, Nichols SJ, et al. Effect of torcetrapib on the progression of coronary atherosclerosis. N Engl J Med 2007;356:1453–60.
21. Kastelein JJ, van Leuven SI, Burgess L, et al. Effect of torcetrapib on carotid atherosclerosis in familial hypercholesterolemia. N Engl J Med 2007;356:5239–30.
22. Harmane L, van Grootheest AC. Pharmacovigilance: methods, recent developments and future perspectives. Eur J Clin Pharmacol 2008;64:743–52.
23. Biomarkers Definitions Working Group. Biomarkers and surrogate endpoints: preferred definitions and conceptual framework. Clin Pharmacol Ther 2001;69:89–95.
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