Preparation of the Rutin-SBA-16 Drug Delivery System

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Abstract

This study sets out a scheme for a controlled release delivery system using SBA-16 as a carrier matrix and Rutin as a drug (Rutin-SBA-16). Physico-chemical characterizations were performed to confirm the structure of the SBA-16 for post-synthesis by scanning electron microscopy (SEM), Transmission Electron Microscopy (TEM) and X-ray Diffraction (XRD). The presence of Rutin-SBA-16 was confirmed by Fourier-transform infrared spectroscopy (FTIR) and Nitrogen adsorption-desorption isotherms at 77 K. The dissolution kinetics was evaluated by the Zero Order, First Order and Higuchi models, and Rutin quantification was carried out by High Performance Liquid Chromatography (HPLC). The best impregnation time, which was 8 hours, adsorbing 284 µg Rutin per mg of silica, and the maximum degree of dissolution occurred in a period of 20 - 25 h. The release kinetics of the Rutin was called Higuchi, and showed high linearity, with a correlation coefficient (R²) of 0.999 compared with 0.905 and 0.980 of the zero order and first order models respectively. The study shows the benefits of Rutin-SBA-16 as a drug delivery system.

Keywords

Rutin, Controlled Release Systems, Kinetic Study, Mesoporous Silica, Flavonoid

1. Introduction

When administered in oral dosage forms, for example in tablets, drug absorption
depends on the ability of the drug to be released from the formulation and to
dissolve under physiological conditions, as well as on its permeability along the
gastrointestinal tract [1]. This ability of the drug to be released (i.e. its availabili-
ty) is assessed through dissolution studies, which allow the release profile of a
drug to be inferred from its parent pharmaceutical form by conducting an anal-
ysis at predetermined times. Through the obtained data, the key parameters for
the availability of the active principle can be estimated, and thus allow a qualita-
tive and quantitative evaluation of some of the formulations [2].

When a drug is administered, only a part of the dose reaches the desired goal,
and a larger amount is spread to other tissues before reaching the target, this
means your metabolism or excretory function can be affected before the drug
reaches the site of action [3]. This has become a serious problem in the treat-
ment of various diseases such as cancer and leishmaniasis, in which the treat-
ment itself is painful, owing to the serious adverse effects that can be attributed
to the lack of specificity and uneven distribution of the drug [4] [5].

One strategy that can solve this type of problem may be the use of a drug de-

delivery system (DDS), that is based on an array of drugs that is capable of con-
voying a modified-release dosage to the target tissue and cells [6]. This involves
employing a particulate carrier matrix system, in which the drug can either be
scattered or retained in the matrix, encapsulated in the core or adsorbed on the
surface. The advantages of DDS are as follows 1) it keeps a constant level of the
drug in the body; 2) it reduces the risk of a dose either being too high or too low;
3) it reduces the number of times required for administration; 4) it provides a
better use of active agents and other factors. All of this add to the comfort of the
patients and improve the effectiveness of the treatment [7].

The array used in the DDS must comply with a number of requirements be-
fore it can be considered to be efficient. It must be biocompatible, able to en-
capsulate or incorporate a high volume of drug dose, allow premature drug re-
lease, have the ability to get to a particular tissue and enable the drug to be re-
leased in a controlled manner [8]. Several arrays are currently being studied
which have a potential use in DDS, such as polymeric micelles, dendrimer, chi-
tosan nanoparticles, mucoadhesive nanoparticles and mesoporous materials,
each with their own particular features and specificity [7] [9].

It should be noted that the mesoporous materials have gained prominence
since they can be used as carrier matrices [10]. The organized structure of the
mesoporous materials makes them useful for several applications, including the
ability to serve as a matrix in the drug delivery system (DDS). Among the me-

soporous materials, silica has become a good candidate because it has excellent
properties such as an orderly mesoporous structure, adjustable pore diameters
and volumes, a large surface area and the presence of silanol groups on the pore
surface, atoxicity, and biocompatibility. As well as this, its surface can be mo-
dified to the controlled process of adsorption and the kinetics of drug release [8]
[11].

Among the support materials studied in catalytic reactions, mesoporous sili-
cas such as MCM ("Mobil Composition of Matter") and SBA ("Santa Barbara Amorphous") silicates have been shown to be good supports because of their large surface area, \( (i.e. \sim 1000 \text{ m}^2\text{g}^{-1}) \), adjustable pore sizes \( (i.e. 2.0 - 10.0 \text{ nm}) \) and uniform pore size distribution \[12\] \[13\]. However, the SBA-16 is regarded as one of the most valuable mesostructures, since it has a cubic 3D arrangement of mesopores in the form of a cage corresponding to a spatial area of \( 1 \text{m}^3_\text{m} \), which have high thermal stability and are generally synthesized in a low pH solution \[14\] \[15\]. For this reason, the organized structure of the SBA-16 materials provides them with useful features for several applications, including the matrix in the drug delivery systems.

This study sets out a scheme for a controlled release system using SBA-16 as a carrier matrix and Rutin as drug. Rutin \( (\text{C}_{27}\text{H}_{30}\text{O}_{16}, \text{molecular mass 610.52 g·mol}^{-1}) \) (Figure 1) is a flavonoid extracted from plants, such as Fava d’anta \( (\text{Dimorphandra mollis Benth}) \), a Brazilian species of the Brazilian Cerrado (the vast tropical savanna region in Brazil), of the legume family \( (\text{Leguminosae}) \) \[16\]. The Rutin is known for its multiple pharmacological properties, such as antitumor, antioxidant, anti-inflammatory, anti-depressant and antiviral activity, and cardioprotective mechanisms. It also has a beneficial effect by 1) reducing the concentration of low density cholesterol; 2) taking action to strengthen the structure of the blood vessel wall layers by making the veins more resistant and 3) overcoming problems related to poor blood circulation \[17\]. Thus, the combination of the essential properties of mesoporous silica with natural products has aroused interest in studies concerned with the spread of these molecules from a controlled release system.

### 2. Materials and Methods

#### 2.1. Reagents and Solvents

Cetrimonium bromide—CTAB (BioXtra, ≥99%, Sigma), Tetraethoxysilane—TEOS (Reagent grade, 98%, Aldrich), Pluronic® F-127 (Powder, BioReagent, Sigma), Deionized water (Milli-Q, Millipore), Hydrochloric Acid—HCl (P.A. 37%, Vetec), Rutin hydrate (≥94% HPLC, powder, Sigma), Sodium lauryl sulfate—SLS (Vetec); Acetonitrile (UV HPLC spectroscopic, 99.9%, J.J. Baker); Methanol (UV HPLC 99.9%, Vetec); Acetic Acid (UV HPLC, spectroscopic 99.9%, Vetec).

#### 2.2. Synthesis, Sample Preparation and Analysis

For the synthesis of mesoporous silica SBA-16, 180 mL of HCl (0.4 mol·L\(^{-1}\)), 1.40 g of Pluronic F-127 surfactant and 0.16 g of the CTAB co-surfactant were diluted in a beaker with 80.0 mL of deionized water for 20 minutes to form the micelles on a magnetic stirrer (TMA10CF Thelga) \[14\]. After the complete dissolution of the surfactant, 5.0 mL of the TEOS silica precursor was added, and kept under vigorous stirring with a mechanical stirrer (713 Fisatom), for 5 minutes. The material was then kept for 5 days at 95.0°C in a thermostated ultrasonic bath.
(MA 185 Marconi). Subsequently, the obtained material was washed, filtered and placed in an oven (Fanem 515) at 60.0°C for 12 h to evaporate the water. With regard to the removal of the surfactant and formation of the mesopores, calcination was carried out in a muffle furnace (MA 385/3 Marconi), with a heating rate of 1.0°C·min⁻¹ until the temperature reached 500°C, where the material remained for 3 hours and was subjected to the characterization of Rutin and an impregnation test.

After the synthesis of SBA-16 was completed, optimization tests were carried out to impregnate Rutin on silica. During this procedure, 50.0 mg of silica in 3.0 mL of the methanolic solution (i.e. methanol/deionized water 1:1 v v⁻¹) of 70.0 mmol·L⁻¹ Rutin (n = 3) was kept under magnetic stirring in a sealed vessel. The methanol was chosen because it is the solvent in which the Rutin has the best solubilization. These samples were kept under stirring for up to 24 h. At the end of every 2 h, the supernatant containing the synthesized material was filtered (using an analytical hydrophilic PTFE syringe filter for 0.45 μM) and oven dried at 60.0°C and submitted to the Rutin-SBA-16 characterizations and kinetic release study.

The Rutin quantification in the impregnation and dissolution stages was carried out by High Efficiency Liquid Chromatography—HPLC (Thermo Scientific Finnigan Surveyor) equipped with a Phenomenex Gemini column (NX 5 μm, C18 110 Å, 150 × 4.6 mm) and UV-VIS detection system at a wavelength of 254 nm. The mobile phase consisted of acetonitrile and water acidified with 1.0% acetic acid. The mobile phase flow was 1.4 mL per minute. The volume injected was 20.0 μL and the retention time of the routine was 3 minutes. The accuracy of the quantification method by HPLC was determined by carrying out addition and recovery tests for 5.00, 15.00 and 30.00 μg·mL⁻¹ of Rutin in a solution prepared in 1% HCl and 1% DDS to simulate the pH of the stomach (i.e. site of interest of the Rutin release activity) and check any possible interference in the readings.

The tests of the impregnated Rutin were run with 50.0 mg of silica (n = 3) in 3.0 mL of methanol solution of 70 mmol·L⁻¹ Rutin which were performed for a period of 24 hours (30 min, 1 h, 2 h, 4 h, 6 h, 8 h, 12 h and 24 h), following centrifugation, 1 mL of each solution was subjected to HPLC analysis. The assay of
Rutin liberation was run with 50.0 mg of silica (n = 3) containing the equivalent amount, impregnated with 14.2 mg of Rutin, was dissolved (Logen Scientific Instruments Dissolution Tester) in 390 mL solution of 1.0% HCl and 1.0% SLS. The solution was kept under stirring at 100 rpm at a temperature of 37.0°C. At intervals of 2 h, 4 h, 6 h, 8 h, 12 h, 18 h and 24 h, aliquots of 5.0 ml were removed and subjected to centrifugation. Subsequently, 1 mL of each aliquot was subjected to HPLC analysis. The dissolution kinetics was evaluated by the Zero Order, First Order and Higuchi models [18] [19] [20].

2.3. Physicochemical and Morphological Characterization

The physicochemical characterizations were performed to confirm the structure of the SBA-16 post-synthesis by scanning electron microscopy—SEM (Jeol JSM-6380 LV), Transmission Electron Microscopy TEM (CM20, Phillips) and X-ray Diffraction—XRD (Bruker D8 Advance).

The SEM characterization was carried out by micrographs obtained by means of the scanning electron microscopy technique, operating at 15 and 30 kV. The samples were metallized with gold for 5 minutes, 30 mA current and 200 mTorr vacuum on a metallizer (Denton Vacuum Desk III).

The TEM was obtained by high voltage, operating up to 200 kV, and electron source LaB6 (lanthanum hexaboride). The particles were dispersed in ethanol and sonicated for 1.5 h in an ultrasonic bath (LimpSonic, LS-3DA-2/X) to obtain the micrographs. The images were captured with a 2 k × 2 k CCD camera, using Digital Micrograph software.

The pore geometry and the distance between its centers were obtained by an X-ray diffraction with CuK α radiation (λ = 1.5418 Å), a Ni filter and a 0.4 mm slit, operating at 40 kV with a current of 40 mA, and an increment of 0.01˚ (in 2θ); a goniometer velocity 1˚·min −1 was applied, and sample scanning in the range of 2θ from 0.7˚ to 5˚.

Rutin impregnation on silica (Rutin-SBA-16) was confirmed by Fourier-transform infrared spectroscopy—FTIR (FTIR Spectrometer, Bomem MB-Series) and Nitrogen adsorption-desorption isotherms at 77 K (Micromeritics® ASAP2020 adsorption). The FTIR spectra for calcined SBA-16 and Rutin-SBA-16 were obtained by dispersing the material in KBr pellets; the spectral range analyzed was 400 to 4000 cm−1.

The Brunauer-Emmett-Teller method—BET [21] [22], was used for specific surface area analysis (SBET) and pore diameter (DP) through N₂ adsorption-desorption experiments at a constant temperature of 77 K. The calcined silica sample was previously degassed at 150°C for 20 hours and the sample containing Rutin was degassed at 60.0°C for 20 hours.

3. Results and Discussion

3.1. Physicochemical and Morphological Characterization

Through the micrographs shown in Figure 2, it can be observed that the par-
articles have a rhombododecahedra morphology that is consistent with the findings of the literature used for the synthesis of this material [14] [15]. The comments in the micrographs obtained by TEM (Figure 3(a) and Figure 3(b)) are in accordance with this structure (SBA-16). Although it does not show the regular and perfect form of a polyhedron, it is possible that the images are becoming similar to those in the pore system [14] [23] [24].

The X-ray diffraction enabled us to calculate the geometrical pattern of the pores and the distance between their centers. The values of the interplanar distances (dhkl) for all the peaks, were obtained by the Bragg equation [25] [26]. The Miller indices were observed in (110), (200), (211) and (220); these peaks are in the range of 0.90˚ - 1.70˚, with a peak of greatest intensity in 2θ around 0.91˚ and a₀ = 13.7 nm) (a₀ = unit cell parameter calculated from d-spacings for Im3m) (Figure 4). The mesoporous silica synthesized presented a porous three-dimensional arrangement of the cubic space group Im3m, and, then, the body-centered cubic structure of mesoporous silica was confirmed by the XRD analysis [24] [25].

The quantification of impregnated Rutin in the SBA-16 and the evaluation of the dissolution kinetics were carried out by HPLC. The external calibration method was applied to HPLC for the Rutin quantification by using the peak area. The linear range of the calibration curve was 2.5 - 50.0 µg·mL⁻¹, and obtained a linear coefficient (R²) of 0.9993. The limits of detection and quantification were evaluated from the data of the analytical curve of Rutin in 1.0% HCl and SLS 1.0%, and obtained values of 0.02 µg·mL⁻¹ and 0.07 µg·mL⁻¹, respectively. The recoveries obtained were 95.00%, 102.50% and 103.60% and the accurate rates,
The amount of impregnated Rutin was quantified by measuring the difference of the initially added Rutin concentration of the supernatant obtained by HPLC. The mechanism through which Rutin interacts with SBA-16 is made possible by the interactions of silanol groups on the surface of silica with the OH groups of the Rutin molecule [27]. The hydrophilicity of disaccharide of Rutin molecules combined with their hydroxyl groups, enhance the Rutin interaction with OH surface silica groups through a hydrogen bond and van der Walls interactions, shown in Figure 5 [27] [28] [29]. The best impregnation time, which was 8 hours, was obtained by adsorbing 284 μg rutin per mg of silica. The Rutin was released after the impregnation test.

A comparison of the FTIR spectrum of silica impregnated with Rutin with calcined silica is shown in Figure 6. This evaluation includes the vibrational modes of the functional groups of silica and Rutin [30] [31] [32]. The bands in 3400, 1635, 1080, 949 and 800 cm$^{-1}$ can be attributed to the $\nu$H-O-H, $\delta$H-O-H, $\nu$Si-O-Si, $\delta$Si-OH and $\nu$Si-O-Si vibrational modes respectively—for the SBA-16. While the presence of the Rutin is confirmed by the bands in 1466 and 1355 cm$^{-1}$ that can be attributed to ($\delta$C-H), the bands of 2971, 2921, 2881 cm$^{-1}$ can be attributed to stretching ($\nu$C-H), which indicates an effective impregnation of Rutin on SBA-16.

The characterizations were finalized by conducting tests involving the adsorption-desorption isotherm of N$_2$ to 77 K to calculate the pore diameter and compare the calcined silica and silica impregnated with Rutin (as in Figure 7(a) and Figure 7(b), respectively). The profile of the isotherms did not change after impregnation, and the structural features of the mesoporous synthesized array were preserved [33]. The comparison of the results of the calcined silica with silica impregnated with Rutin provided the measurements of the specific surface area (SBET), pore diameter (DP) and pore volume (VP), which were 732 m$^2$·g$^{-1}$, 6.6 nm, 0.55 cm$^3$·g$^{-1}$ respectively for Rutin-SBA-16. These data demonstrate that there was a reduction in surface area and pore volume, thus confirming the
presence of Rutin on silica (i.e. SBET, DP and VP of 806 m$^2$·g$^{-1}$, 6.6 nm, 0.60 cm$^3$·g$^{-1}$) to SBA-16 [14] [24]. The comparison between the DP of SBA-16 and Rutin-SBA-16 shows that the pore diameter did not change; this can be explained by the fact that the Rutin is impregnated inside the pores and not necessarily in the walls of the pore, which would not result in a change in the diameter. This might indicate a non-uniform distribution of Rutin within the silica pores [27].

Figure 5. Schematic representation of the interaction of Rutin with the silica surface.

Figure 6. FTIR spectrum of calcined silica and silica impregnated with Rutin.

Figure 7. N$_2$ sorption isotherm at 77 K of SBA-16 material, with pore size distribution (diameter) included, (a) SBA-16 sample; (b) SBA-16 sample-Rutin.
After the physicochemical characterization of Rutin-SBA-16, there were kinetic studies of controlled release for the models of Zero Order, First Order and Higuchi, as shown in Table 1.

3.2. Kinetic Release Study of Rutin-SBA-16

Kinetic studies are widely used to assist in the development of new formulations, assess the influence of changes in the production process and/or in the formulation, monitor quality control from batch to batch of a particular specialist area, and make an evaluation of pharmaceutical equivalence between the presentations of different manufacturers.

The dissolution profile of Rutin that has been evaluated in this work is shown in Figure 8. It is clear from this that the maximum release occurs between 20 - 25 h. The release kinetics of the Rutin are called Higuchi (Table 1), and have a high degree of linearity, with a correlation coefficient (R²) of 0.999, as opposed to 0.905 and 0.980 of the zero order and first order models respectively.

In the case of the zero order model, the form of dosage does not fragment (i.e. it maintains its initial area and does not reach a state of equilibrium) by releasing the drug gradually [18] [31] [34]. With regard to the first-order model, the dissolution profiles are already suitable since the pharmaceutical forms contain water-soluble drugs in porous matrices. In this case, the drug is released in proportion to the

![Figure 8. Release profile of Rutin solution.](image)

Table 1. Types of dissolution kinetics models.

| Kinetic Model | Equation | Description | Plot Graph | Ref. |
|---------------|----------|-------------|------------|------|
| Zero order    | \( C = C_0 + K_0 t \) | Where, \( C_0 \) is the initial concentration of drug at time \( t = 0 \), \( K_0 \) is zero order rate constant, \( t \) is the time taken for \( C \) amount of drug release | Cumulative % drug release vs. time | Okano et al., 1987; Yin et al., 2009; Park, 2014 |
| First order   | \( \log C_t = \frac{(\log C_0 - k_1 t)}{2.303} \) | Where, \( C_t \) is amount of drug released in \( t \) time and \( C_0 \) is the initial amount of drug, \( K_1 \) is first order rate constant | Log % of drug remaining vs. time and the slope of the plot gives the first order rate constant | Hallam et al., 1983; Shah and Rajput, 2017; Mucientes and Peña, 2009 |
| Higuchi       | \( Q = K_H t^{1/2} \) | \( K_H \) is Higuchi dissolution constant, \( Q \) is the amount of drug released in time \( t \) per unit area | Cumulative % drug release vs. square root of time | Gouda et al., 2017; Higuchi, 1963; Siepmann and Peppas, 2011 |
amount that still remains, and at the same time, the released amount decreases over the course of the testing period [19] [34] [35].

The Higuchi release systems are for uncoated devices which are often used to describe the rate of the controlled release of the drug from a matrix system; this is because the yield of the drug is based on Fick’s first law of diffusion which is proportional to the square root of time [2] [35] [36]. In this case, the release of the Rutin-SBA-16 occurs by diffusion of the Rutin through the matrix pores by means of the monolithic system, where the interactions that occur between the silica and the Rutin are of the hydrogen bond type [37].

In light of the study material, someone weighing 70 kg would require the ingestion of approximately 30 mg, (i.e. Rutin-SBA-16 containing 120 μg·kg⁻¹ Rutin) for effective anticancer treatment involving the inhibition of cell proliferation and removal of reactive oxygen species that can cause DNA damage and lead to mutations in a dosage [37]. Although supplementary toxicity tests are needed, the study shows the benefits of Rutin-SBA-16 as a drug delivery system. Since the SBA-16 mesoporous silica of this research represents an interesting carrier matrix for modulating rutin release (Higuchi Model). This ability of silica to modulate release will allow in vivo studies to evaluate different pharmaceutical forms for dose/frequency adequacy of rutin use.

4. Conclusion

The techniques of characterization provided proof that the array of mesoporous silica (SBA-16) was prepared successfully. Impregnation of Rutin on silica was confirmed from the FTIR techniques and the adsorption/desorption of nitrogen. The kinetic tests showed high linearity, with a correlation coefficient (R²) of 0.999 for the Higuchi model. This was due to the diffusion of Rutin by the pores of the array through the monolithic system, where the interactions that occur between silica and Rutin are of the hydrogen bond type. The Rutin-SBA-16 system released 284 μg of Rutin by mg of silica in a period of 24 h. Moreover, it was able to provide a controlled release of the drug and included an array for future tests of toxicities and in vivo applications.

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Conflicts of Interest

The authors declare no conflicts of interest regarding the publication of this paper.

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