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BİLİR, AYKUT; EMÜL, EZĞİ; and SAĞLAM, NECDET (2020) "Development of albumin macroinitiator for polymers to use in DNA origami coating," Turkish Journal of Medical Sciences: Vol. 50: No. 5, Article 37. https://doi.org/10.3906/sag-2001-245
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Development of albumin macroinitiator for polymers to use in DNA origami coating

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Background/aim: DNA nanostructures have many advantages over polymers and lipid based drug delivery agents such as biodegradability and biocompatibility. However their transfection rates and stability still limit their wide use in nanomedicine. In this study highly versatile and straightforward albumin coating preparation method is showed for DNA nanostructures.

Materials and methods: N-methylolmaleimide was esterified with a-bromoisobutyrl bromide (BiBB) to achieve bromine functional structure. Then it was attached to bovine serum albumin (BSA) via cysteine-maleimide bond further to use as macroinitiator for atom transfer radical polymerization (ATRP). Cationic polymers can be synthesized from this end further to use as binding domain for fabricated 60 Helix bundle DNA origami.

Results: Proton nuclear magnetic resonance (¹H NMR) analysis used for characterization. Methyelene group hydrogens’ peak in 5.0 ppm and strong peak in 1.5–2.0 ppm range showed proper methylolation of maleimide and bromine functional formation, respectively. Then BSA-macroinitiator formation is verified by 1780 Da peak shift in MALDI-TOF (Matrix-assisted laser desorption/ionization - time of flight) spectrum. Moreover electrophoretic mobility shift assay (EMSA) showed successful dense 60 Helix bundle formation.

Conclusion: In this study, a facile method is developed to synthesize protein conjugated-ATRP initiator further can be used in polymerization and coating DNA nanostructures. It is feasible for any protein containing cysteine amino acid.

Keywords: DNA origami, bionanotechnology, atom transfer radical polymerization, drug delivery

1. Introduction

Structural DNA nanotechnology has made considerable development since Seeman proposed using DNA as a building material for bottom-up self-assembly in 1982 [1]. DNA origami is the common technique to form 2- and 3-dimensional nanostructures with exceptional complexity in which a long single-stranded DNA is being folded by hundreds of distinct complementary short ‘staple’ strands [2–5]. It is employed in numerous applications such as biosensors [6,7], advanced drug delivery [8], synthetic ion channels [9], molecular size electronic circuits [10] and plasmic nanostructures [11].

In addition, these structures are highly suitable for nanomedicine applications thanks to their size (10–100nm). They are inherently biocompatible, nontoxic, biodegradable, have low immunogenicity and can enter cells without transfection agents [12–17]. Numerous smart drugs carriers have developed so far to deliver molecules include fluorescent dyes [18], anticancer drugs [19, 20], CpG (unmethylated cytosine-phosphate-guanine dinucleotides) [14], siRNA [21], enzymes [22]. Despite these unique properties of DNA nanostructures, there are still 2 key challenges to overcome the limiting factors of their extensive usage. Firstly, due to negatively charged hydrophilic nature of DNA origami it shows low cell-transfection rates [23]. Secondly, these structures are often sensitive to cellular medium and depletion of salt ions; although they are slightly stable in cell lysates [24] and can resist nuclease action [25], an efficient method to improve their stability in vivo is urgently needed.

In order to increase the stability and transfection rates of DNA nanostructures, various materials and protection techniques suggested such as liposome encapsulation [26] and polymer coating [27–31], backbone modification [32], spermidine stabilization [33]. It has been shown that transfection rates can be improved by utilizing DNA intercalators as surface modification agents [34], virus protein [35] and specific proteins studied so far [36]. However, taking into account the accessibility, selectivity and immune responserserum albumin is an easily accessible candidate for coating. Serum albumin is the most abundant blood protein, and has long serum half-life and widely used in clinically approved applications in drug delivery [37,38]. The thiol-maleimide chemistry is frequently used
for specific conjugation utilizing cysteine residue in serum albumin [39–42]. Many techniques used to synthesize polymers with protein reactive groups [43–45]. Grafting from approach is the more recent method for synthesizing polymeric biomaterials [46]. By creating specific sites on biomacromolecules, living radical polymerization can be initiated and broad range of protein-polymer conjugates can be achieved. Consequently, by coating DNA nanostructures with serum albumin, can these structures’ stability and transfection rates to the cells be increased?  

In this study, BSA transformed into macroinitiator for atom transfer radical polymerization (ATRP) by targeting the free cysteine residue as reactive towards the maleimide. This initiator can be used for having cationic polymer and utilized as a binding domain that can be further attached to the negatively charged DNA origami surface. It is believed that this method will broaden applications of DNA origami in nanomedicine as a novel alternative to the nanoparticle and lipid based drug delivery carriers.

2. Materials and methods
In this study by coating DNA nanostructures with cationic polymer armed albumin protein it is expected to increase these structures’ stability and transfection rates to the cells. The procedure is as follows: using maleimide as a starting material and modifying it to have hydroxyl group. Then from this functional group, a-bromoisobutyryl bromide covalently bonded by esterification. After that bromine functional maleimide conjugated with bovine serum albumin (BSA) by cysteine-maleimide bond. Then ATRP was performed from this macroinitiator by using 2-(dimethylamino) ethyl methacrylate (DMAEMA) as monomer. 60 Helix bundle DNA origami prepared by thermally annealing the scaffold by 141 distinct short staple strands.

Maleimide supplied from Alfa Aesar [Thermo Fisher (Kandel) GmbH, Kandel, Germany]. Formaldehyde, α-bromoisoobutyryl bromide (BiBB), bovine serum albumin, 2-(dimethylamino) ethyl methacrylate (DMAEMA) monomer, ethidium bromide (EthBr) and agarose were purchased from Sigma-Aldrich Chemie GmbH (Taufkirchen, Germany). Milli-Q purified water was used. Scaffold for 60 Helix bundle DNA origami was purchased from TilibitNanosystems (München, Germany) and staple strands from Integrated DNA Technologies Inc. (Coralville, IA, USA). 10x TAE buffer supplied from USB Corporation (Cleveland, OH, USA). Proton nuclear magnetic resonance (1H NMR) spectra were recorded with Bruker Avance 400 MHz (Bruker BioSpin Corporation, Billerica, MA, USA). The chemical shift calibration performed using residual CDCl3 peaks. MALDI-TOF analyses were performed with an UltrafleXtreme 2000 Hz (Bruker Daltonics, Bremen, Germany) with a SmartBeam II laser (355 nm) and operated in positive mode.

2.1. Synthesis of N-substituted maleimide derivative
N-methylolmaleimide was synthesized according to the method Tawney et al. proposed (Figure 1) [47]. At room temperature 90 mL of 5% sodium hydroxide was added to a suspension of 2.910 g of maleimide in 5.559 g of 37% formaldehyde (final pH » 5). Within 10 min all of maleimide was dissolved and a mildly exothermic reaction occurred. Separation of the product was begun promptly. After leaving for 2.5 h at room temperature, the solution was filtered. One recrystallization from ethyl acetate ended 1.12 g of product and it was dried under vacuum to remove solvent.

Bromine functional maleimide was prepared by esterification of N-methylolmaleimide with a-bromoisobutyryl bromide according to the method of Çakır et al. (Figure 2) [48]. Under nitrogen, 1.24 mL (2.307 g, 10 mmol) a-bromoisobutyryl bromide was added dropwise to a stirring mixture of NMM (1 g, 8 mmol) and triethylamine (1.37 mL, 10 mmol) in 23.3 mL of CHCl3 in an ice bath for 1 h. After complete addition of the acid bromide, the reaction was stirred at room temperature for 3 h. A dark red reaction mixture observed and it was washed with water (3 × 23.3 mL) and then dried over MgSO4. After filtration and evaporation of CHCl3, it was dried under vacuum and recrystallized from ethanol.

2.2. BSA-macroinitiator
Synthesis of BSA-macroinitiator targeted the free cysteine residue (Cys-34) as reactive towards the maleimide, described earlier by Nicolas et al. (Figure 3) [49]. BSA (34 mg, 0.52 μmol) was dissolved in 4.6 mL of 100 mM
phosphate buffer (pH = 7.0). A solution of 12.2 mg of N-substituted maleimide derivative in 0.2 mL of DMSO was added to this slowly. The mixture was gently stirred during 24 h at ambient temperature and the solid residue was then removed by centrifugation. The supernatant was diluted with deionized water and dialyzed with a 12,000–14,000 Da molecular weight cut-off (MWCO) membrane against deionized water for 3 days. The solution was then lyophilized to isolate the BSA-macroinitiator.

2.3. Atom transfer radical polymerization (ATRP)
BSA-polymer conjugate achieved via ATRP from BSA macroinitiator, by using modified method of Välimäki et al. (Figure 4) [50]. CuBr (53 mg, 0.37 mmol) was placed in a round-bottom flask with a stirring bar. BSA macroinitiator (25 mg, 0.37 mmol) and ligand HMTETA (170 mg, 0.74 mmol) dissolved in 10 mL of water and purged with nitrogen gas for 15 min. Then the solution transferred to the flask by cannula. The same procedure repeated for DMAEMA (5.8 g, 37 mmol) and the polymerization was performed for 4 h in a sealed flask at room temperature with magnetic stirring. For 240 min, every 30 min sample was taken from the flask to vials, then they were opened to air and placed in an ice bath to stop the reaction. The solid residue was removed by centrifugation, and the supernatant was lyophilized to give blue product.

2.4. Preparation of DNA origami nanostructure
60 Helix bundle DNA origami nanostructure was prepared, purified and characterized as described earlier [51,52]. Briefly, folding solution obtained by mixing following substances:
- 20 mL M13mp18 scaffold (100 nM)
- 40 mL staples (500 nM)
- 40 mL folding buffer containing 2.5 TAE, 12.5 mM NaCl and 50 mM MgCl₂

Then final solution was annealed by G-Storm thermocycler (Gene Technologies Ltd., Melbourne, Australia). The excess amount of staples was removed by PEG-based purification. Folding and purification of DNA origami is characterized by agarose gel electrophoresis.

**Figure 2.** Esterification of N-methylolmaleimide with BiBB.

**Figure 3.** Thioether bond formation between cysteine-maleimide derivative.

**Figure 4.** ATRP of BSA-polymer conjugate.
3. Results and discussion

Similar results observed with the literature in the methylolation of maleimide, maleimide quickly dissolved, and gave an endothermic reaction [47]. Thin layer chromatography of maleimide and methylolation step product confirmed the proper methylolation of maleimide. Maleimide runs faster than N-methylolmaleimide and was observed under UV light (Figure 5). The structure of N-methylolmaleimide was confirmed by 1H NMR recorded in CDCl₃ as well. 1H NMR spectrum displays signals corresponding to hydrogens of methylene group and hydroxyl group thus proves the proper methylolation of maleimide (Figure 6). 1H NMR (CDCl₃), d (ppm): 3.01–3.05 (t, 1H), 5.00–5.04 (d, 2H), 6.70–6.72 (s, 2H).

To validate the structure of bromine functional maleimide (MBr), 1H NMR spectrum recorded in CDCl₃. The resonance signals and relative intensities corresponding to methylene (–CH₂) and methyl (–CH₃) groups evidenced successful esterification, denoted in b and c respectively and it is found compatible with the results reported earlier (Figure 7) [48]. 1H NMR (CDCl₃), d (ppm): 1.82–1.85 (s, 6H), 5.56–5.57 (s, 2H), 6.77–6.78 (s, 2H). Conjugation of bromine functional maleimide (MBr) to BSA was demonstrated by MALDI-TOF. Incubation of BSA with MBr showed a shift to position 68413 m/z (Figures 8A and 8B). This corresponds to a change of 1780 Da and proves proper conjugation of bromine functional maleimide (MBr) to BSA (Figure 8). Polymerization from BSA macroinitiator was followed by 1H NMR. In order to be ensure the complete dissolution of the sample, 0.7 mL CDCl₃ mixed with 0.3 mL CD₃OD and used as solvent. The resonance signal corresponding to repeating unit (methylene) group of PDMAEMA was searched around 1.0 ppm, however no peak observed in after 30 min (Figure 9A), 240 min. (Figure 9B), 240 min and dilution with water 1:1 volumetric ratio (Figure 9C). This can be attributed to side reaction between functional groups on amino acid residues and DMAEMA monomer. Moreover, the mechanism can be slow due to the big structure of BSA, and 240 min is not enough to observe the polymer peak on 1H NMR spectrum. To overcome this issue, different polymerization medium and ratios of the substances will be tried. Gel electrophoretic mobility shift assay (EMSA) verified that folded and compact 60HB runs faster than the scaffold as shown in (Figure 10). Besides, PEG purification step removed the excess staples efficiently. However there may be some possible limitations in the study such as in MALDI-TOF analysis chemical shift between BSA and BSA macroinitiator comparison, it is unclear the ratio of one to one chemical conjugates to the electrostatically gathered structures.

4. Conclusion

As a conclusion, we demonstrated a facile and widely applicable method to prepare BSA macroinitiator that can be further used in preparation of polymeric biomaterials. Characterization stages have given valuable information about transformation of maleimide to bromine functional initiator and thioether formation by Michael addition of maleimide end to thiol of cysteine residues. Though the weak polymer peak for backbone in 1H NMR spectrum, a clear shift in MALDI-TOF spectra has provided an evidence for protein-initiator binding. In this method, any cysteine containing proteins can be selectively conjugated with bromine functional ATRP initiator, however polymerization medium and ratios of the substances will be taken into account to avoid denaturation of protein. Therefore, this approach offers notable opportunities which can be extended not only for DNA origami coating but also for responsive biohybrid material development. This method makes considerable contribution for attracting the attention to DNA origami studies and to future studies with BSA-like biocompatible proteins and polymers.

Acknowledgments/disclaimers

Aykut Bilir gratefully acknowledge Finnish National Agency for Education for their scholarship. Ezgi Emül. and Aykut Bilir thank Turkish Council of Higher Education for scholarship. The work was carried out under the Academy of Finland’s Centres of Excellence Programme (2014–2019). The authors wish to thank Biohybrid Materials Group members at Aalto University, SallaVälimäki for help during macroinitiator synthesis, Heiniljäsf for characterization in DNA origami studies and Dr. Mauri A. Kostiainen for helpful discussions.

Conflict of interest

The authors declare no conflict of interest.

This study was presented at the Taiwan-Turkey Science Summit entitled “Translation of Cells, Nanomaterials and Signaling Molecules into Regenerative Medicine” between April 1 to 3, 2018.
Figure 6. 1H NMR spectrum of N-methylolmaleimide.

Figure 7. 1H NMR spectrum of bromine functional maleimide (MBr).
**Figure 8.** MALDI-TOF spectra of A) BSA and B) BSA macroinitiator.

**Figure 9.** Resonance signals of according to chemical shifts shown in ppm in NMR spectra of samples taken from polymerization medium after A) 30 min, B) 240 min C) 240 min and dilution with water 1:1 volumetric ratio.
Figure 10. Electrophoretic mobility shift assay (EMSA) results for folded and purified 60HB DNA origami.
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