Right ventricular function in hypertrophic cardiomyopathy: A speckle tracking echocardiography study

Altuğ Cincin, Kırsat Tigen, Tansu Karaahmet 1, Cihan Dündar 2, Emre Gürel 2, Mustafa Bulut 2, Murat Sünbül, Yelda Başaran

Department of Cardiology, Faculty of Medicine, Marmara University; İstanbul-Turkey
1Department of Cardiology, Faculty of Medicine, Acıbadem University; İstanbul-Turkey
2Department of Cardiology, Kartal Koşuyolu Heart Training and Research Hospital; İstanbul-Turkey

ABSTRACT

Objective: The aim of this study was to explore right ventricular (RV) mechanical function in patients with hypertrophic cardiomyopathy (HCM) by 2-D speckle tracking echocardiography (2-D-STE).

Methods: Forty-three patients with HCM (mean age 48, 17 females) and 40 healthy subjects were consecutively included in this cross-sectional study. The diagnosis of HCM was based on the presence of typical clinical, electrocardiographic (ECG), and echocardiographic features. Patients with LV systolic impairment, significant valvular disease, history of coronary artery disease, hypertension, malignancy, and chronic obstructive pulmonary disease were excluded. Right and left ventricular (LV) function was assessed by tissue Doppler imaging (TDI) and 2-D-STE. Hypertrophic cardiomyopathy patients were divided into two groups according to ACC/ESC guidelines (LVOT gradient below and above 30 mm Hg). Student t-test was used to compare differences between groups. Non-parametric tests (Mann-Whitney U) were used in cases of abnormal distribution.

Results: Hypertrophic cardiomyopathy patients had a significantly larger right atrium and RV diameters compared to controls. Mean pulmonary artery pressures (mPAP) were significantly higher in HCM patients (19.01±13.09 mm Hg vs. 8.40±4.50 mm Hg; p<0.001). Although RV Sm measurements were similar, RV strain measurements (-28.51±5.36% vs. -32.06±7.65%; p=0.016) were significantly lower in HCM patients. Left ventricular global longitudinal, radial, and circumferential strain values were also significantly different between the two groups (-20.50±3.58% vs. -24.12±3.40%; p<0.001, 38.18±12.67% vs. 44.80±10.15%; p=0.012, -21.94±4.28% vs. -23.91±3.95%; p=0.036 consecutively). Rotational movement of LV in each apical, mid-, and basal left ventricular segment was determined, and only mid-ventricular rotation of the HCM patients was more clockwise (-1.71±2.16 ° vs. 0.04±1.72 °; p<0.001). Although mPAP measurements were higher in HCM patients with significant LVOT obstruction (21.52±13.26 mm Hg vs. 12.31±10.53 mm Hg; p=0.049), none of the other TDI or 2-D-STE parameters was significantly different between groups.

Conclusion: Speckle tracking echocardiography-derived right ventricular systolic function is impaired in HCM patients when compared with healthy subjects. However, RV systolic function is not affected form LVOT obstruction and left ventricular rotation dynamics in HCM patients. (Anatol J Cardiol 2015; 15: 536-41)

Keywords: hypertrophic cardiomyopathy, right ventricular function, speckle tracking echocardiography

Introduction

Hypertrophic cardiomyopathy (HCM) is one of the primary diseases of the heart, characterized by impaired myocardial function despite increased left ventricle (LV) wall thickness (1). As the anatomical proximity emerges a clear functional relationship between two ventricles and genetic basis of the disease targets whole myocardium, right ventricular (RV) functional impairment accompany with the disease (2-4). However, evaluation of RV function with conventional echocardiographic techniques is unreliable because of the complex RV geometry, resulting in conflicting data.

Novel echocardiographic techniques offer reliable, reproducible, and quantitative information about right ventricle functions. Tricuspid annular systolic velocity (s) by TDI is well correlated with RV ejection fraction (EF), and isovolumic acceleration during isovolumic contraction (IVA) is proposed to be a useful index of RV contractile function and likely to be unaffected by preload and afterload changes in a physiological range (5, 6). Two-dimensional (2-D) speckle tracking echocardiography (2-D-STE) is an echocardiographic technique that uses standard 2-D images for detecting speckles (acoustic backscatters) in a previously determined region and is followed frame by frame (7). Multiple studies have demonstrated the utility of 2-D-STE in the
evaluation of RV function without the limitation of a Doppler beam angle (8, 9). 2-D-DSTE was found to be a prognostic and clinical valuable tool in many heart diseases involving or affecting the RV (10-12).

The aim of our study was to evaluate RV functions in patients with obstructive and non-obstructive HCM and explore whether RV systolic function was affected by the disease itself or abnormal LV mechanics by using TDI and 2-D-DSTE parameters.

**Methods**

Fifty-six consecutive HCM patients underwent a clinical and echocardiographic examination in this cross-sectional study between 2010 and 2011 at Department of Cardiology, Faculty of Medicine, Marmara University. The diagnosis of HCM was based on the presence of typical clinical, electrocardiographic (ECG), and echocardiographic features, with global or segmental ventricular myocardial hypertrophy (diastolic wall thickness ≥15 mm), occurring in the absence of any other cardiac or systemic disease, such as Fabry's disease and cardiac amyloidosis (13).

Exclusion criteria were LV systolic impairment [ejection fraction (EF) <55%], significant valvular disease, history of coronary artery disease, hypertension, malignancy, chronic obstructive pulmonary disease, any arrhythmia that should affect echocardiographic measurements, and poor echocardiographic image quality. The study protocol was approved by the Ethic Committee.

Thirteen patients were excluded because of the criteria listed above, and 43 HCM patients were enrolled in the study; 40 healthy volunteers without any cardiac or systemic disease were matched for age and sex and included in the control group. Obstructive HCM was defined (in accordance with the latest American College of Cardiology guidelines) by the presence of a peak instantaneous gradient greater than 30 mm Hg from the ventricular cavity to the aorta under basal conditions (13).

**Echocardiographic examination**

All patients underwent a complete echocardiographic study with a commercially available echocardiography device (Vivid 7, GE Vingmed Ultrasound AS, Horten, Norway) by a single experienced cardiologist. Data acquisition was performed with a 3.5-MHz transducer at a depth of 14-18 cm in the parasternal and apical views (standard parasternal short-axis from basal, midventricular, and apical levels; apical long-axis; two-chamber; and four-chamber views). Standard M-mode, 2-D, and color-coded tissue Doppler images (TDIs) were obtained during breath-hold, stored in cine-loop format from 3 consecutive beats, and transferred to a workstation for further offline analysis (EchoPAC 6.1; GE Vingmed Ultrasound AS). Gain settings, filters, and pulse repetitive frequency were adjusted to optimize color saturation, and a color Doppler frame scanning rate of 100-140 Hz was used for color TDI. Cardiac dimensions were measured according to the guidelines of the American Society of Echocardiography, and LV EF was calculated by biplane Simpson’s method (14). Mean pulmonary artery pressure (mPAP) was calculated with the acceleration time of the pulmonary artery velocity (Pact) by the Mahan formula [mPAP (mm Hg)=79-(0.62 x Pact (msn))] (15).

Pulsed TDI was performed to assess LV and RV longitudinal functions. In the apical four-chamber view, a 5-mm pulsed Doppler sample volume was placed on basal septum, basal lateral wall, and lateral tricuspid annulus. Settings were adjusted for a frame rate between 120 and 180 Hz, Nyquist velocity range of ±20 cm/s, and horizontal record velocity of 90-100 m/s. Peak systolic velocity of the basal septum, basal lateral wall, and tricuspid lateral annulus (s); early and late diastolic velocities of LV septum and lateral wall; and isovolumetric contraction time (IVCT) and peak myocardial velocity during isovolumetric contraction (IVV) of the tricuspid lateral annulus were measured. LV systolic and early and late diastolic velocities were calculated by averaging the basal septal and lateral values. Isovolumetric acceleration (IVA) was calculated as the mean slope of the IVV wave (IVV/IVCT, m/s²) (6).

Multidirectional analysis of the LV [in the radial (GRS), circumferential (GCS), and longitudinal (GLS) directions] and RV strain was performed using 2-D speckle tracking imaging, as previously described (16-18). The assessment of GRS and GCS in the LV was performed by applying 2-D speckle tracking imaging to the parasternal short-axis views at a frame rate of 70-90 frame/s. The mid-ventricular short axis of the LV was divided into six segments, and the values of GRS and GCS were derived from the average of the six segmental peak systolic strain values. The assessment of longitudinal peak systolic strain was performed by applying 2-D speckle tracking imaging to the apical two- and four-chamber views of the LV. The LV was divided into six segments in each apical view. The values of GLS were derived from the average of the six segmental peak systolic longitudinal strain values.

Two-dimensional speckle tracking analysis of the parasternal SAX views at the base and at the apex revealed LV ‘rotation’ and ‘rotation rate’ curves as the angular displacement and the velocity of displacement of the LV around its central axis. Negative values indicated clockwise rotation, while positive values indicated counterclockwise rotation. Left ventricular ‘twist’ and ‘twist rate’ were defined as the net difference of LV peak systolic ‘rotation’ and ‘rotation rate’ between basal (clockwise) and apical (counterclockwise) short axis planes.

Values were expressed in ‘degree (°)’ and ‘°/s’ respectively. ‘Untwist’ was expressed as a diastolic angular motion of the LV, opposite to twist. ‘Untwisting rate’ (°/s) was defined as the peak twist rate during early diastole. Midrotation was examined to detect the “null velocity” segment within the left ventricular cavity. The difference between left ventricular left ventricular mid and basal segment and basal segment rotation values was defined as midrotation, indicating the net twist between these segments.

For RV analysis, the free wall endocardial border of the ventricle, manually tracked on the end-systolic frame, and epicardial border were detected by the software. Strain curves and per-
percentage of longitudinal differences at the basal segment of the RV free wall were obtained automatically (Fig. 1) (19, 20).

**Statistical analysis**

All statistical tests were performed with a commercially available statistical analysis program (SPSS 15.0 for Windows; SPSS, Inc., Chicago, IL, USA). All continuous variable results were checked for normal distribution by the Kolmogorov-Smirnov test and presented as mean±standard deviation (SD) or median (minimum-maximum values), while categorical variables were expressed as ratios. Student t-test was used to compare difference between groups. Non-parametric tests (Mann-Whitney U) were used in cases of abnormal distribution. Correlation analysis was performed by Spearman’s correlation test. A p value of <0.05 was determined as statistically significant. Intraobserver (the mean difference between two independent measurements) and interobserver (the mean difference between two independent observers) variabilities were analyzed in 10 randomly selected studies and expressed as the mean percent error (difference divided by number of observations).

**Results**

Forty-three patients with HCM (mean age 48, 17 females) and 40 healthy subjects (mean age 47, 19 females) were included in the study. Demographic and conventional echocardiographic parameters are presented in Table 1. The groups were not significantly different in terms of cardiovascular risk factors. Interventricular septum (IVS) and posterior wall measurements in the HCM group were 22.51±5.81 mm and 12.81±3.91 mm, respectively. Left ventricular ejection fraction values were not different between HCM patients and the control group.

Doppler, TDI, and 2-D-STE results of the groups are shown in Table 2. Estimated mPAP was higher in HCM patients (19.01±13.09 mm Hg vs. 8.40±4.50 mm Hg; p<0.001). Although RVs (11.62±2.66 cm/s vs. 12.40±2.22 cm/s; p=0.153) and IVV (7.97±3.32 cm/s vs. 8.97±2.83 cm/s; p=0.154) measurements were similar, IVA (1.89±0.74 cm/s² vs. 2.48±0.67 cm/s²; p=0.001) and strain measurements of the basal RV free wall (-28.51±5.36% vs. -32.06±7.65%; p=0.016) were significantly lower in HCM patients. The estimated inter- and intra-observer variability for RVs and strain of basal RV free wall measurements were 2.3% and 3.1% versus 2.8% and 3.4%, respectively. Left ventricular GLS, GRS, and GCS values between groups were also significantly different (-20.50±3.58% vs. -24.12±3.40%; p<0.001) and interobserver (the mean difference between two independent observers) variabilities were analyzed in 10 randomly selected studies and expressed as the mean percent error (difference divided by number of observations).

**Table 1. Basic clinical and echocardiographic parameters of the groups**

| Parameter | Patients with HCM (n=43) | Controls (n=40) | P |
|-----------|--------------------------|-----------------|---|
| Age, years | 47.79±14.94 | 46.57±11.18 | 0.678 |
| Female sex | 17 | 19 | 0.464 |
| BSA, m² | 1.85±0.21 | 1.79±0.18 | 0.222 |
| IVS, mm | 22.51±5.81 | 10.06±1.46 | <0.001 |
| PW, mm | 12.81±3.91 | 9.86±1.56 | <0.001 |
| LVEDD, mm | 42.55±6.40 | 45.99±3.85 | 0.004 |
| LVESD, mm | 24.37±5.33 | 27.03±3.52 | 0.009 |
| EF, % | 73.69±9.10 | 71.15±5.78 | 0.135 |
| E/A ratio | 1.13±0.49 | 1.46±1.45 | 0.168 |
| DT, ms | 195±57 | 200±35 | 0.642 |
| E/e ratio | 19.8±8.6 | 9.6±2.7 | <0.001 |
| LVs, cm/s | 5.55±1.46 | 7.76±1.68 | <0.001 |
| LVe, cm/s | 5.02±2.10 | 9.38±2.18 | <0.001 |
| LVA, cm/s | 5.82±1.87 | 8.01±2.12 | <0.001 |
| RA area, cm² | 12.97±2.24 | 11.91±2.65 | 0.055 |

**Table 2. Doppler and 2D-STE indices of the groups**

| Parameter | Patients with HCM (n=43) | Controls (n=40) | P |
|-----------|--------------------------|-----------------|---|
| Pacc, ms | 96.75±21.12 | 113.86±7.27 | <0.001 |
| mPAB, mm Hg | 19.01±13.09 | 8.40±4.50 | <0.001 |
| RVs, cm/s | 11.62±2.66 | 12.40±2.22 | 0.153 |
| RV IVV, cm/s | 7.97±3.32 | 8.97±2.83 | 0.154 |
| RV IVA, cm/s² | 1.89±0.74 | 2.48±0.67 | 0.001 |
| RV BLS, % | -28.51±5.36 | -32.06±7.65 | 0.016 |
| LV GLS, % | -20.50±3.58 | -24.12±3.40 | <0.001 |
| LV GRS, % | 38.18±12.67 | 44.80±10.15 | 0.012 |
| LV GCS, % | -21.94±4.28 | -23.91±3.95 | 0.036 |
| LV rot-apical, ° | 15.93±7.16 | 15.84±5.38 | 0.952 |
| LV rot-mid, ° | -1.71±2.16 | 0.04±1.72 | <0.001 |
| LV rot-basal, ° | -6.38±2.90 | -6.75±3.33 | 0.594 |
| LV twist, ° | 22.37±6.77 | 22.29±6.22 | 0.955 |
| LV untwist, °/s | -122.57±51.72 | -135.64±38.93 | 0.209 |
38.18±12.67% vs. 44.80±10.15%; p=0.012, -21.94±4.28% vs. -23.91±3.95%; p=0.036, consecutively). Rotational movement of the LV in each apical, mid-, and basal segment was determined, and only mid-ventricular rotation of the HCM group patients was more clockwise in the HCM group (-1.71±2.16° vs. 0.04±1.72°; p<0.001).

Hypertrophic cardiomyopathy patients were divided into two groups according to their LV outflow tract gradient. Thirty-two of the 43 HCM patients whose peak LVOT gradients were higher than 30 mm Hg, were assigned as obstructive. Echocardiographic findings of obstructive and non-obstructive patients are shown in Table 3. Pulmonary acceleration time (92.70±21.39 ms vs. 107.55±16.99 ms; p=0.049) and mPAP measurements (21.52±13.26 mm Hg vs. 12.31±10.53 mm Hg; p=0.049) were higher in HCM patients with LVOT obstruction. Tissue Doppler and STE measurements of RV did not reveal significant difference between obstructive and non-obstructive HCM patients according to an LVOT gradient threshold of 30 mm Hg. RVs (11.71±2.55 cm/s vs. 11.36±3.10 cm/s; p=0.099), and IVA (1.88±0.77 cm/s² vs. 1.92±0.72 cm/s²; p=0.887) were similar. Strain measurements of the basal RV free wall (-27.95±5.36% vs. -30.15±5.26%; p=0.246) were similar between the two groups.

Another comparison was performed by separating HCM patients according to their direction of mid-ventricular rotation. Counter-clockwise rotation was seen in 8 of the 43 patients, and clockwise rotation was seen in the remaining patients. There was no difference between the two groups in terms of RV functional parameters. Right-sided echocardiographic parameters were evaluated according to mid-ventricular rotation quartiles. Table 4 shows the comparisons between quartiles. Among the evaluated parameters, no significant difference was detected between mid-ventricular rotation quartiles or the 1st and 4th quartiles.

**Table 3. Doppler and 2D-STE indices of HCM patients, according to LV outflow gradients**

| Parameters                  | Patients with obstruction (n=32) | Patients without obstruction (n=11) | P   |
|-----------------------------|---------------------------------|------------------------------------|-----|
| Pacc, ms                    | 92.70±21.39                     | 107.55±16.99                       | 0.049|
| mPAB, mm Hg                 | 21.52±13.26                     | 12.31±10.53                        | 0.049|
| E/A ratio                   | 1.09±0.45                       | 1.23±0.59                          | 0.432|
| E/e ratio                   | 20.4±9.4                        | 18.3±7.2                           | 0.496|
| LVs, cm/s                   | 5.78±1.52                       | 4.88±1.08                          | 0.078|
| LVe, cm/s                   | 5.17±2.29                       | 4.58±1.41                          | 0.427|
| LVA, cm/s                   | 6.07±1.93                       | 5.09±1.56                          | 0.137|
| RVS, cm/s                   | 11.71±2.55                      | 11.36±3.10                         | 0.714|
| RV IVV, cm/s                | 8.01±3.13                       | 7.86±3.96                          | 0.899|
| RV IVA, cm/s²               | 1.88±0.77                       | 1.92±0.72                          | 0.887|
| RV BLS, %                   | -27.95±5.36                     | -30.15±5.26                        | 0.246|
| LV GLS, %                   | -20.31±3.37                     | -21.07±4.28                        | 0.550|
| LV GRs, %                   | 38.31±13.62                     | 37.86±10.31                        | 0.923|
| LV GCS, %                   | -22.35±4.33                     | -20.87±4.12                        | 0.336|
| LV rot-apical, °            | 16.68±6.92                      | 16.60±8.07                         | 0.720|
| LV rot-mid, °               | -1.92±2.16                      | -1.16±2.17                         | 0.331|
| LV rot-basal, °             | -6.23±3.09                      | -6.76±2.44                         | 0.741|
| LV twist, °                 | 22.52±6.48                      | 21.99±6.53                         | 0.728|
| LV untwist, °/s             | -132.78±41.00                   | -122.53±53.78                      | 0.343|

**Table 4. Doppler and 2D-STE indices of HCM patients, according to interquartile ranges of mid-ventricular rotation values**

| Parameters                  | 1. Quartile (n=10) | 2. Quartile (n=10) | 3. Quartile (n=10) | 4. Quartile (n=10) | P (overall) | P (1st and 4th quartiles) |
|-----------------------------|-------------------|-------------------|-------------------|-------------------|-------------|--------------------------|
| Pacc, ms                    | 107.50±18.3       | 90.30±62          | 98.33±16.00       | 91.62±19.38       | 0.317       | 0.130                    |
| mPAB, mm Hg                 | 12.35±11.39       | 23.20±18.98       | 18.03±9.92        | 22.19±12.01       | 0.317       | 0.130                    |
| RVs, cm/s                   | 11.94±2.68        | 10.98±2.33        | 12.29±2.57        | 11.26±3.18        | 0.715       | 0.739                    |
| RV IVV, cm/s                | 7.75±3.00         | 7.04±3.37         | 7.87±4.04         | 8.72±3.05         | 0.714       | 0.573                    |
| RV IVA, cm/s²               | 2.18±0.72         | 1.62±0.68         | 1.60±0.87         | 2.23±0.56         | 0.134       | 0.696                    |
| RV BLS, %                   | -28.26±0.30       | -27.35±5.36       | -30.36±4.82       | -27.55±4.09       | 0.359       | 0.529                    |

**Discussion**

In our study, significant impairment in RV function was demonstrated in HCM patients by using 2-D-STE when compared with age- and sex-matched healthy volunteers. Although tissue Doppler-derived systolic velocity of the tricuspid lateral annulus did not differ between groups, 2-D-STE-based strain of the RV free wall basal segment in the HCM group was lower in HCM patients. Although the calculated mPAP values were higher, patients who had LVOT outflow tract obstruction were found to have similar RV systolic function parameters compared to patients without LVOT obstruction. Mid-ventricular rotation of the LV was significantly clockwise in HCM patients compared to controls but similar between obstructed and non-obstructed HCM patients. HCM patients were analyzed according to their...
RV function is affected in HCM as a consequence of the direct disease itself, ventricular interdependence, or dynamic afterload changes (2, 21-23). Although the morphological and physiological changes of the LV in HCM are well described, the right heart is obscured by its complex geometry and physiology (24, 25). The clear prognostic importance of RV function in various diseases has encouraged investigations about new echocardiographic methods for accurate diagnosis of RV failure (26-28). In a recently published article, D’andrea et al. (29) showed that 2-D-STE-derived RV myocardial systolic deformation is influenced in HCM patients. There was a negative association between inter-ventricular septal thickness and RV global longitudinal strain in HCM patients. Our results also suggested impairment in STE-derived RV systolic function when compared with normal subjects.

**LV obstruction and right heart functions**

In patients with HCM and LVOT obstruction, increased LV loading conditions and diastolic dysfunction have an important effect in RV workload (30). A study in patients treated with alcohol septal ablation showed that eliminating LVOT obstruction was related with decreased PAP and increased RV ejection fraction values (31). In our study, patients with LVOT obstruction had higher pulmonary artery pressures. However, TDI- or 2-D-STE-based RV systolic function parameters were similar between obstructed and non-obstructed patients. This might be due to mild elevation of pulmonary artery pressures in our HCM patients. LVOT obstruction was not related with impairment in LV strain and rotation parameters in our patient group. This might preserve the left atrial and pulmonary artery pressures and maintain RV systolic function within normal limits. Our findings need to be clarified by further large-scale follow-up studies.

**Mid-ventricular rotation and right ventricle functions**

In a study made by Carasso et al. (32), HCM patients with preserved systolic function were associated with impaired STE-derived LV longitudinal strain, unchanged LV torsion, and increased circumferential strain. However, mid-ventricular mechanical analysis of HCM patients revealed a clockwise rotation pattern, despite “mid-ventricular null velocity.” To the best of our knowledge, this is the first study evaluating the effect of this diversity on RV functions. In our study, similar to the Carasso et al. (32) results, mid-cavity rotational motion was significantly different between control and HCM patients. However, RV systolic function was not affected from the mid-ventricular rotation pattern. A detailed analysis was performed by dividing the HCM group into mid-rotation quartiles, which showed similar RV strain values. Preservation of LV systolic parameters and a mild elevation in pulmonary artery pressures might be an explanation for these findings. The relation between mid-rotation and RV systolic parameters in HCM patients with advanced disease indicates further research.

**Study limitations**

The main limitation of our study was the small sample size. Although the difference in RV BLS between HCM patients and controls was significant, whole measurements were within the normal range, as previously established (33). The importance of these sub-clinical findings should be determined with a prospective study, including prognosis.

Morphologic changes in the RV itself are another important factor affecting functions in HCM patients, but these changes were not considered in the present study. Cardiac MRI might be used to validate both RV systolic functions and morphologic changes, like fibrosis.

**Conclusion**

Speckle tracking echocardiography-derived right ventricular systolic function is impaired in HCM patients when compared with healthy subjects. However, RV systolic function is not affected form LVOT obstruction and left ventricular rotation dynamics in HCM patients.

**Conflict of interest:** None declared.

**Peer-review:** Externally peer-reviewed.

**Authorship contributions:** Concept - Y.B., K.T.; Design - K.T.; Supervision - A.C., T.K.; Data collection and/or processing - C.D., A.C., E.G.; Analysis and/or Interpretation - M.B., A.C., M.S.; Literature search - T.K.; Writing - A.C., K.T.; Critical review - Y.B.

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