Suppression of Fibrotic Reactions of Chitosan-Alginate Microcapsules Containing Porcine Islets by Dexamethasone Surface Coating

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Background: The microencapsulation is an ideal solution to overcome immune rejection without immunosuppressive treatment. Poor biocompatibility and small molecular antigens secreted from encapsulated islets induce fibrosis infiltration. Therefore, the aims of this study were to improve the biocompatibility of microcapsules by dexamethasone coating and to verify its effect after xenogeneic transplantation in a streptozotocin-induced diabetes mice.

Methods: Dexamethasone 21-phosphate (Dexa) was dissolved in 1% chitosan and was cross-linked with the alginate microcapsule surface. Insulin secretion and viability assays were performed 14 days after microencapsulation. Dexa-containing chitosan-coated alginate (Dexa-chitosan) or alginate microencapsulated porcine islets were transplanted into diabetic mice. The fibrosis infiltration score was calculated from the harvested microcapsules. The harvested microcapsules were stained with trichrome and for insulin and macrophages.

Results: No significant differences in glucose-stimulated insulin secretion and islet viability were noted among naked, alginate, and Dexa-chitosan microencapsulated islets. After transplantation of microencapsulated porcine islets, nonfasting blood glucose were normalized in both the Dexa-chitosan and alginate groups until 231 days. The average glucose after transplantation were lower in the Dexa-chitosan group than the alginate group. Pericapsular fibrosis and inflammatory cell infiltration of microcapsules were significantly reduced in Dexa-chitosan compared with alginate microcapsules. Dithizone and insulin were positive in Dexa-chitosan capsules. Although fibrosis and macrophage infiltration was noted on the surface, some alginate microcapsules were stained with insulin.

Conclusion: Dexa coating on microcapsules significantly suppressed the fibrotic reaction on the capsule surface after transplantation of xenogenic islets containing microcapsules without any harmful effects on the function and survival of the islets.

Keywords: Diabetes mellitus; Islets of Langerhans transplantation; Dexamethasone; Cell encapsulation; Fibrosis
INTRODUCTION

Type 1 diabetes is an autoimmune disease resulting from β-cell destruction, in which patients are incapable of maintaining euglycemia without insulin injection [1,2]. Islet transplantation is an alternative method of exogenous insulin that can allow insulin secretion depending on glucose level [3,4]. Since the introduction of the Edmonton protocol based on immunosuppressants of daclizumab, sirolimus, and tacrolimus, human islet transplantation has increased [5,6]. However, the graft failure rate remains high at up to 90% at 5 years after transplantation [7]. In addition, immunosuppressants could have an adverse effect on islet function and survival [8,9]. Treatment with tacrolimus and sirolimus reduces islet size and induces islet apoptosis in rats [8]. In humans, these drugs disrupt insulin granule formation and insulin processing via cleavage at dibasic sites and upregulate amyloid deposition [9].

One of the promising methods to avoid immune attack after islet transplantation is to microencapsulate islets to protect islets from immune response-mediated destruction. Microencapsulation can allow penetration of small molecules, such as oxygen, nutrients, and insulin, while preventing pass-through of high molecular weight components, such as immunoglobulin and macromolecules [10]. Many researchers have studied capsular materials, such as alginate, collagen, and silica. Among them, alginate microcapsules are a common technique based on poly-L-lysine used to protect transplanted islet grafts [11,12]. However, this approach has a limitation of fibrosis on the microcapsule surface, which is induced by the immune response of the host via macrophages and small molecule antigens. The fibrotic reaction on the capsular surface influences the permeability of the capsules and thus inhibits nutrient and oxygen exchange. This reaction induces hypoxia and destruction of encapsulated islets, leading to necrosis of islets and graft failure [13].

To improve biocompatibility and subsequently reduce fibrosis associated with microcapsules, various anti-inflammatory drugs have been applied as a strategy to minimize host response and enhance the stability of transplantable microcapsules [14,15]. Dexamethasone 21-phosphate (Dexa) is a commonly used anti-inflammatory drug that potently suppresses inflammatory pathways. Dexa has been reported to suppress the immune reaction of transplanted devices by selective suppression of pro-inflammatory factors, such as macrophages [16]. Dexa also prevents the proliferation of fibroblasts in mice [17] and pulmonary fibrosis induced by bleomycin [18]. However, high-dose systemic administration of Dexa could impair islet function and survival [19-21]. In contrast, a low dose of Dexa improves islet survival and preserves islet revascularization [13]. Therefore, we aimed to improve the biocompatibility and fibrosis of microcapsules by Dexa surface coating on alginate.

METHODS

Animals

The Seoul National University (SNU) designated pathogen free (DPF) pigs aged at least 6 months were used as xenogenic islet donors [22]. Male alpha 1, 3-galactosyltransferase knock-out mice (GalT KO) aged 7 to 12 weeks (kindly provide from Prof. Chung-Gyu Park, SNU) were used as recipients. Type 1 diabetes was confirmed with a portable glucometer (GLUCOCARD X-METER, Arkray, Kyoto, Japan); if random blood glucose levels from the tail vein exceeded 300 mg/dL for three consecutive days after intraperitoneal one-shot injection of 200 mg/kg dose of streptozotocin (STZ, Sigma-Aldrich, St. Louis, MO, USA; freshly dissolved in 0.01 M citric acid buffer, pH 4.5), the diagnosis of type 1 diabetes was made. The GalT KO mice were maintained at a constant temperature in a cycle of 12 hours of light followed by 12 hours of dark and provided with laboratory chow and water. All of surgical interventions and presurgical and postsurgical animal care were provided in accordance with the Laboratory Animals Welfare Act, the Guide for the Care and Use of Laboratory Animals and the Guidelines and Policies for Rodent Survival Surgery provided by the IACUC (Institutional Animal Care and Use Committee) in College of Medicine, The Catholic University of Korea (approval number: CUMS-2014-0105-02).

Materials

Pronova ultrapure low viscosity guluronic acid (UP-LVG) sodium alginate (20 to 200 kDa) was purchased from Pronova (Novamatrix, Sandvika, Norway). Povidone was purchased from Sungkwangpham (Cheonan, Korea). Acridine orange (AO), magnesium sulfate (MgSO₄), magnesium chloride (MgCl₂), sodium phosphate monobasic (NaH₂PO₄), sodium chloride (NaCl), chitosan (from crab shells, minimum 85% deacetylated), barium chloride (BaCl₂), nicotineamidine, 4-(2-hydroxyethyl)piperazine-1-ethanesulfonic acid (HEPES), propidium iodide (PI), STZ, luria/miller agarose (LB agarose), paraformaldehyde (PFA), fluorescein isothiocyanate (FITC)-labeled dextran, sodium hydroxide (NaOH), H₂O₂, potassium chloride (KCl), calcium chloride (CaCl₂), gluconic acid, potassium hydroxide (KOH), L-histidine, D-mannitol, sodium pyruvate, monobasic potassi-
Um phosphat (KH₂PO₄), citric acid, 4′-6-diamidino-2-phenylindole (DAPI), hydrochloric acid (HCl), sodium bicarbonate (NaHCO₃), 3,3′-diaminobenzidine (DAB), harris hematoxylin, dithizone (DTZ), mayer’s hematoxylin, biebrich scarlet aqueous, acid fuchsin, glacial acetic acid, phosphotungstic acid, light green, and OptiPrep™ were purchased from Sigma Aldrich. Dulbecco’s phosphate-buffered saline (DPBS), RPMI 1640, Media 199 (M199), fetal bovine serum (FBS), antibiotic/antimycotic solution, gentamycin, and porcine serum (PS) were obtained from Gibco (Carlsbad, CA, USA). Dextra was purchased from Jeil pharm (Seoul, Korea). Cefazolin was purchased from ChongKunDang (Seoul, Korea), ketamine HCl from Yuhan Corporation (Seoul, Korea), CIzyme collagenase MA and CIzyme BP protease from VitaCyte (Indianapolis, IN, USA) and Phenol red free 1×Hank’s balanced salt solution (1×HBSS; without Ca²⁺, Mg²⁺) was purchased from WelGENE Inc. (Gyeongsan, Korea).

Islet isolation procedure

Porcine islets were isolated from SNU DPF adult pigs according to established protocols [22,23]. After cannulation of the pancreatic duct using cold histidine-tryptophan-ketoglutarate (HTK) solution (Custodiol™, Koehler Chemi, Bensheim, Germany), the pancreas was delivered in cold HTK solution. The delivered pancreas was washed sequentially with 1% cold povidone, a cold solution of antibiotics (0.2% cefazolin, 0.016% gentamycin dissolved in DPBS), and cold DPBS. Washed pancreas was trimmed to remove non-pancreatic tissues in cold HTK solution, then CIzyme collagenase MA and CIzyme BP protease from VitaCyte (Indianapolis, IN, USA) and Phenol red free 1×Hank’s balanced salt solution (1×HBSS; without Ca²⁺, Mg²⁺) were purchased from WelGENE Inc. (Gyeongsan, Korea).

Islet microencapsulation procedure

Alginate solution for microencapsulation was prepared that 2% (w/v) UP-LVG alginate was dissolved in Ca²⁺-free Krebs–Ringer–HEPES buffer (KRH buffer: 135 mM NaCl, 4.7 mM KCl, 25 mM HEPES, 1.2 mM KH₂PO₄, 1.2 mM MgSO₄). After 1 to 2 days in cultured, the isolated SNU DPF porcine islets were suspended in a solution of 2% UP-LVG alginate and at a concentration of 10,000 IEq/mL for SNU DPF porcine islets. Microcapsules were made with a coaxial bead generator (Nisco Engineering Inc., Zürich, Switzerland) that expelled islet-solution mixture using a syringe pump (Harvard apparatus, Holliston, MA, USA) into a 150 mm petri-dish (SPL, Pocheon, Korea) of NaCl, 10 mM BaCl₂ solution (10 mM BaCl₂, 2 mM KCl, 135 mM NaCl, 10 mM HEPES, pH 7.4). The encapsulated islets were washed with 1×HBSS and 1 mg/mL Dextra contained pH 4.5% filtrated chitosan solution (w/v in deionized distilled water) for 10 minutes with stirring for Dexa-chitosan coating. Chitosan, high affinity positive charged residue [24], was used as an intermediary to link alginate and Dexa because both alginate and Dexa have negative charges.

All these procedures are made at room temperature. After chitosan coating, microcapsules were washed 3 to 4 times with 1×HBSS and cultured in M199 supplemented with 10% PS, 16 mM nicotinamide, 24 mM NaHCO₃ and 1% penicillin/streptomycin at 37°C in humid conditions with 5% CO₂.

Confirm of microcapsules morphology and pore size

Dextra-chitosan-coated alginate surface was observed using transmission electron microscopy (TEM; JSM-1010, JEOL Ltd., Tokyo, Japan). Microcapsule pore size was determined by the diffusion FITC-labeled dextran conjugates of various sizes [25]. Alginate and Dextra-chitosan-coated alginate microcapsules were incubated for 3 days in 1×HBSS with FITC-labeled dextran conjugates (4, 10, 20, 40, 70, 150, 250 kDa). After incubating, each microcapsule was imaged under a confocal fluorescence microscope (AxioVert 200TM, Carl Zeiss, Oberkochen, Germany).
In vitro dexamethasone 21-phosphate release test
The standard curve was produced by dissolving Daxa in 1 × HBSS; a range of 0 to 500 µg/mL was obtained. The standard Daxa concentration was measured using a UV/Vis spectrometer (Nanodrop, Thermo Fisher Scientific, Waltham, MA, USA) at an absorption wavelength of 240 nm. The 1,000 ea Daxa-chitosan-coated alginate microcapsules were incubated in a 100 mm petri-dish with 10 mL 1 × HBSS solution, at 37°C under humid conditions with 5% CO₂, for the Daxa release test. After 35 days, 10 µL supernatant samples were obtained from the incubated petri-dish and measured using the same UV/Vis wavelengths as the standard preparation spectrometer [26]. A regression analysis of the in vitro Daxa release was used to determine the following equation for the Daxa standard curve: Y = [0.412 × X (R²=1.000)], where Y is the concentration of Daxa (µg/mL), X is the value of the absorbency of Daxa, and R² is the regression coefficient.

Microencapsulated islets viability measurement
The standard AO/PI method was used to evaluate islet viability 0, 1, 3, 5, 7, and 14 days after microencapsulation. Naked, alginate microencapsulated, and Daxa-chitosan-coated alginate microencapsulated islets were incubated in 1 × HBSS with 1% FBS with AO/PI for 10 minutes. Viability of these islets was evaluated using AO/PI double staining to observe viable (AO; green) and dead cells (PI; red) with an inverted fluorescence microscope (Observer.Z1, Carl Zeiss).

Glucose stimulated insulin secretion test
Tests were performed on islet samples of 100 IEq (150 to 250 µm diameter islet selection) for each group. Islet samples were transferred to a 60 mm petri-dish (SPL) and incubated in a 5 mL 1% FBS contained glucose-free Krebs-Ringer-Bicarbonate buffer (KRB buffer: 24 mM NaHCO₃, 5 mM KCl, 115 mM NaCl, 2.5 mM CaCl₂, 1 mM MgCl₂, 25 mM HEPES) for 1 hour at 37°C in humid conditions with 5% CO₂ before performing the glucose-stimulated insulin secretion (GSIS) test. Then, each group of islets was incubated in a 5 mL 1% FBS contained low-glucose (2.8 mM) KRB buffer for 1 hour 37°C in humid conditions with 5% CO₂. After incubation, each group of islets was washed with an 1% FBS contained glucose-free KRB buffer and incubated in a 5 mL 1% FBS contained high-glucose (16.8 mM) KRB buffer for 1 hour at 37°C in humid conditions with 5% CO₂. The amount of insulin was determined using the human insulin radioimmunoassay kit (RIA kit, Millipore, Burlington, MA, USA).

Transplantation in mouse model
Male GalT KO mice weight 20 to 30 g were used as recipients for each type microencapsulated islet transplantation. Their presence of diabetes was considered if two or more non-fasting blood glucose levels from the tail vein exceed 300 mg/dL after intraperitoneal injection of STZ. Two groups of transplanted animals were studied: (1) alginate microencapsulated islets were transplanted (group 1; n=5); (2) Daxa-chitosan-coated alginate microencapsulated islets were transplanted (group 2; n=6). Microencapsulated islets (10,000 IEq) were slowly infused into the peritoneal cavity via a flank incision. After transplantation, blood glucose levels were monitored every day in the first week and twice a week afterwards. Graft failure was determined if three consecutive non-fasting blood glucose levels exceeds 300 mg/dL.

Fibrosis score calculate
Two hundred and thirty-one days after transplantation, microcapsules were harvested under ketamine HCl anesthesia by peritoneal lavage using warm 1 × HBSS. The harvested microcapsules were stained with DTZ and assessed under an inverted microscope to establish the degree of fibrotic cell infiltration (CKX41, Olympus, Tokyo, Japan). Images were captured by an E330 digital camera (Olympus) connected to the inverted microscope. Fibrosis infiltration score was defined on the harvested microcapsule surface (Fig. 1) [27]. Fibrosis infiltration score = (0×0%/total)+(3.3×<50%/total)+(6.6×>50%/total)+(10×100%/total).

| Portion of microcapsule surface infiltrated by fibrotic cells | 0% | <50% | >50% | 100% |
|-----------------------------|-----|------|------|------|
| Score index                 | 0   | 3.3  | 6.6  | 10   |

Fig. 1. Classification of microcapsules harvested after graft failure in the peritoneal cavity of galactosyltransferase knock-out mice mice based on the extent of fibrotic cell infiltration to the microcapsule surface.
Immunohistochemistry and Masson-Trichrome stain
Harvested microcapsules were fixed 15 to 30 minutes in 4% PFA at 4°C. Fixed capsules were embedded with 5% LB agarose at room temperature for 10 minutes. And, it was sectioned at 4 to 7 μm. Immunohistochemistry staining was conducted using specific antibodies such as insulin, macrophage, CD3. Specimens were incubated overnight at 4°C with diluted primary antibodies (insulin, CD3, macrophage; Abcam, Cambridge, MA, USA), and then incubated for 1 hour with fluorescence-conjugated secondary antibodies (FITC, Rhodamine, Vector Lab, Burlingame, CA, USA) at room temperature. DAPI (Sigma-Aldrich) was employed for nuclear staining. Immunofluorescence was detected under a fluorescence microscope (Observer.Z1). For infiltrated fibrosis on harvested microcapsules stain, deparaffinized specimens were incubated with weigert’s iron hematoxylin at room temperature for 10 minutes. Next, Biebrich scarlet-acid fuchin solution at 15 minutes and 5% aqueous phosphotungstic acid at 3 minutes and 1% glacial acetic acid at 3 minutes. Finally, it was incubated with light green solution at 15 minutes.

Statistical analysis
Results were presented as the mean ± standard error of mean values. Survival rate was analyzed using log-rank test survival curves, differences between two groups were analyzed using the two-tailed unpaired t test using GraphPad Prism version 5.0 (GraphPad software Inc., La Jolla, CA, USA). P value of less than 0.05 was assumed statistical significance.

RESULTS
Characterization of Dexamethasone (Dexa)-chitosan-coated alginate microcapsules
The layer of Dexa-chitosan coating on alginate microcapsules was observed by TEM (Fig. 2A). The permeability of each microcapsule was estimated using a diffusion assay of FITC-labeled dextran molecules of various sizes (Fig. 2B). Dexa-chitosan-coated alginate microcapsules exhibited similar diffusion of FITC-dextran at a molecular weight of 4 to 40 kDa compared with alginate microcapsules. This finding suggests that the Dexa-chitosan coating did not affect the permeability of gas exchange and nutrients through the microcapsule inner core. However, diffusion of FITC-labeled dextran in Dexa-chitosan-coated alginate microcapsules was blocked between 40 and 70 kDa. This finding suggests that the molecular cutoff weight of the capsule membrane is at least 70 kDa, which can prevent immune cells and immunoglobulin G (IgG; 150 kDa) from penetrating into the microcapsules. Dexa release from Dexa-chitosan-coated alginate microcapsules was measured using a UV/Vis spectrometer (Fig. 2C). Dexa release was relatively constant over 35 days after microencapsulation.
Viability and function of microencapsulated islets

The viability of encapsulated islets was confirmed by AO/PI assay on days 0, 3, and 7 after microencapsulation and compared with naked islet viability (Fig. 3A). The survival rate of microencapsulated islets stabilized after 3 days. Fourteen days after microencapsulation, the percentage of PI-positive cells in the Dexcel-tosan-coated alginate group (6.05% ± 1.73%) was similar to that of the alginate group (5.99% ± 0.80%) and did not differ from that of the naked islets (4.13% ± 0.91%) (Fig. 3B). Islet function assessed by GSIS was also similar among naked, alginate, and Dexcel-tosan-coated alginate groups 14 days after microencapsulation. These results suggest that islet viability and function were well maintained after microencapsulation (Fig. 3C).

**Fig. 3.** Viability and secretory function of the microencapsulation islets. (A) Viability of microencapsulated islets based on acridine orange/propidium iodide (AO/PI) staining of naked islets, alginate microcapsules, and dexamethasone (Dexa)-chitosan-coated alginate microcapsules (DCAs) at days 0, 3, and 7. Scale bar = 100 µm. (B) PI-positive cells (%) in naked islets, alginate microencapsulated islets and Dexcel-tosan-coated alginate microencapsulated islets over 14 days. (C) Insulin secretory function of microencapsulated islets during glucose-stimulated insulin secretion. Insulin secretion was significantly increased in response to glucose in all groups. *P<0.05 compared with the naked islets in each date group; bP<0.01.
Improvement of blood glucose levels after Dexa-chitosan-coated alginate microencapsulated islet transplantation in diabetic mice

Before transplantation, the nonfasting blood glucose levels of all diabetic mice were greater than 300 mg/dL. Blood glucose levels significantly decreased after transplantation and remained within the normal range until 231 days after transplantation in both the Dexa-chitosan-coated alginate and alginate groups (Fig. 4A). The average nonfasting blood glucose level for 231 days after transplantation was significantly reduced in the Dexa-chitosan-coated alginate microencapsulated islets compared with the alginate group (176.0 mg/dL vs. 202.7 mg/dL, \(P<0.05\)). The graft survival rate was higher in the Dexa-chitosan-coated alginate microencapsulated islets, but the difference was not significant (log-rank test, \(P=0.228\)) (Fig. 4B).

Fig. 4. Blood glucose level and graft survival in galactosyltransferase knock-out mice (GalT KO) mice transplanted with microencapsulated islets. (A) Change in blood glucose levels in GalT KO mice transplanted with alginate microencapsulated islets (n=5) and dexamethasone (Dexa)-chitosan coated alginate microencapsulated islets (n=6). (B) Graft survival proportions in GalT KO mice transplanted with microencapsulated islets. Graft survival proportions of Dexa-chitosan-coated alginate microencapsulated islets (open circle) improved approximately 60% compared with 20% survival for alginate microencapsulated islets (close circle) (log-rank test, \(P=0.228\)).

Improved fibrosis of Dexa-chitosan-coated alginate microcapsules after transplantation

Pericapsular fibrosis was observed from harvested microcapsules 231 days after transplantation. As shown in Fig. 5A (upper panels), the fibrosis of Dexa-chitosan-coated alginate microencapsulated islets was conspicuously decreased compared with that of the alginate group. The fibrosis infiltration score was significantly reduced in the Dexa-chitosan-coated alginate group compared with the alginate group (176.0 mg/dL vs. 202.7 mg/dL, \(P<0.05\)). The graft survival rate was higher in the Dexa-chitosan alginate group compared with the alginate group, but the difference was not significant (log rank test, \(P=0.228\)) (Fig. 4B).

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DISCUSSION

In this study, we developed Dexa-chitosan-coated alginate microcapsules that have similar properties (capsular pore size, islet viability, and insulin secretion) to alginate microcapsules but improved biocompatibility. After xenogeneic transplantation, blood glucose levels were normalized in both groups, but the mean glucose level was lower in the Dexa-chitosan group compared with the alginate group. The graft survival rate was higher in the Dexa-chitosan group, but not significantly, compared with the alginate group. Pericapsular fibrosis and inflammatory cell infiltration of harvested microcapsules were significantly reduced in Dexa-chitosan-coated alginate microcapsules com-
pared with alginate microcapsules.

The microcapsule has been studied to avoid the immune rejection response from various immune cells, i.e., immunoglobulin and cytokine-induced pathways [28,29]. We previously reported that alginate microencapsulated islets improve blood glucose levels without immunosuppressants in diabetic mice [30]. However, alginate microcapsules have a limitation of perivascular fibrosis in the pericapsular area. The application of anti-inflammatory regimens has the potential to alleviate the immunological response to transplanted medical devices [31] or implanted cell-based therapeutics [32,33]. Dang et al. [34] assessed the immunosuppressive effects of 16 small molecules on the host response to transplanted biomaterials by subcutaneous injection. Among them, Dexa and curcumin effectively suppress early inflammation markers, such as reactive oxygen species and cathepsin activity [34]. In particular, Dexa exhibits a superior reduction in cathepsin activity [34]. Therefore, this study sought to overcome pericapsular inflammation and fibrosis with Dexa-chitosan coating on alginate microcapsules in xenotransplantation.

We previously developed a rapamycin-alginate capsule to improve the biocompatibility of encapsulated islets [35]. Rapamycin-polyethylene glycol-coated alginate microcapsules strongly inhibit fibrosis on the microcapsule surface. However, rapamycin has a limitation that impairs islet function. In contrast to a previous study, the current study demonstrated that Dexa-chitosan-coated alginate microcapsules inhibited inflammatory cell

Fig. 5. Dithizone staining of harvested microencapsulated porcine islets and the measurement of fibrotic cell infiltration to the microcapsule surface. (A) The left panel shows harvested porcine islets with alginate microcapsules, and the right panel shows harvested dexamethasone (Dexa)-chitosan-coated alginate microcapsules. (B) Fibrosis infiltration score of microcapsules compared with alginate- and Dexa-chitosan-coated alginate microcapsules at 231 days after 10,000 IEq islet transplantation. *P<0.05 compared with alginate microcapsules.

Fig. 6. Trichrome or immunohistochemistry staining of harvested encapsulated porcine islets and measurement of fibrotic cell infiltration to the microcapsule surface. (A) Fibrosis infiltrated stain (green) harvested from alginate microcapsules and dexamethasone (Dexa)-chitosan-coated alginate microcapsules. (B) Macrophages (green) and CD3 (red) were stained in alginate microcapsules. Red arrows indicate CD3-positive cells. Scale bar=50 µm. (C) Porcine islets were stained with insulin antibody (red). Scale bar=50 µm. DAPI, 4´6-diamidino-2-phenylindole.
infiltration and fibrosis while preserving islet function. Another study reported improved pericapsular fibrosis and islet viability in alginate microcapsules coated with pentoxifylline, which is known to inhibit the inflammatory response induced by interleukin-2 and tumor necrosis factor-α [36]. However, this finding was only demonstrated in vitro experiments. Therefore, the effects of pentoxifylline-coated alginate capsules on islet function and inflammation should be assessed in an in vivo transplantation model. We demonstrated preserved islet function and improved fibrosis and inflammatory cell infiltration of Dexa-chitosan-coated alginate microcapsules in vitro and in vivo.

Both Dexa-chitosan-coated alginate and alginate microcapsules have the same molecular cutoff weight of 70 kDa. This finding suggests that it can effectively block the penetration of high molecular weight molecules, such as macrophages and IgG, but not small molecules, such as cytokines. The immune response caused by these small molecules induces inflammation, fibrosis and islet damage. In our study, despite improved blood glucose levels, alginate microcapsules showed significant fibrosis and inflammatory cell infiltration on the capsular surface, which could be critical for long-term graft survival and clinical application of transplantation. Meanwhile, these reactions were rarely observed in Dexa-chitosan-coated alginate microcapsules. Our findings suggest that Dexa coating on microcapsules could improve biocompatibility through control of the immune response and increase the potential for clinical application of encapsulated islet transplantation.

In conclusion, Dexa coating on alginate microcapsules significantly suppressed pericapsular fibrosis and inflammatory cell infiltration in microencapsulated islet transplantation. These results suggest that Dexa-chitosan-coated alginate microcapsules potentially represent a promising technology for both xenogeneic islet transplantation. This could also be used for allogeneic islet transplantation that has less immune response than xenogeneic islet transplantation.

**CONFLICTS OF INTEREST**

No potential conflict of interest relevant to this article was reported.

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**AUTHOR CONTRIBUTIONS**

Conception or design: H.S.P., K.H.Y. Acquisition, analysis, or interpretation of data: M.J.K., H.S.P., J.W.K., E.Y.L., M.R., Y.H.Y. Drafting the work or revising: M.J.K., H.S.P., J.W.K., E.Y.L. Final approval of the manuscript: G.K., C.G.P., K.H.Y.

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