Novel description of the large conductance Ca^{2+}-modulated K^{+} channel current, BK, during an action potential from suprachiasmatic nucleus neurons

John R. Clay
National Institute of Neurological Disorders and Stroke, National Institutes of Health, Bethesda, Maryland

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Abstract
The contribution of the large conductance, Ca^{2+}-modulated, voltage-gated K^{+} channel current, I_{BK}, to the total current during an action potential (AP) from suprachiasmatic nucleus (SCN) neurons is described using a novel computational approach. An experimental recording of an SCN AP and the corresponding AP-clamp recording of I_{BK} from the literature were both digitized. The AP data set was applied computationally to a kinetic model of I_{BK} that was based on results from a clone of the BK channel \( \alpha \) subunit heterologously expressed in Xenopus oocytes. The I_{BK} model result during an AP was compared with the AP-clamp recording of I_{BK}. The comparison suggests that a change in the intracellular Ca^{2+} concentration does not have an immediate effect on BK channel kinetics. Rather, a delay of a few milliseconds may occur prior to the full effect of a change in Cai^{2+}. As shown elsewhere, the \( \beta 2 \) subunit of the BK channel in the SCN, which is present in the daytime along with the \( \alpha \) subunit, shifts the BK channel activation curve leftward on the voltage axis relative to the activation curve of BK channels comprised of the \( \alpha \) subunit alone. That shift may underlie the diurnal changes in electrical activity that occur in the SCN and it may also enhance the delay in the effect of a change in Cai^{2+} on BK kinetics reported here. The implication of these results for models of the AP for neurons in which BK channels are present is that an additional time dependent process may be required in the models, a process that describes the time dependence of the development of a change in the intracellular Ca^{2+} concentration on BK channel gating.

Introduction
BK channels are a significant factor underlying membrane excitability of suprachiasmatic nucleus (SCN) neurons (Cloues and Sather 2003; Jackson et al. 2004; Colwell 2006; Meredith et al. 2006; Pitts et al. 2006; Kent and Meredith 2008; Belle et al. 2009; Montgomery and Meredith 2012; Montgomery et al. 2013; Whitt et al. 2016). Specifically, they have been implicated in the diurnal changes in spontaneous firing that occur in the SCN (Colwell 2006; Meredith et al. 2006; Whitt et al. 2016). SCN neurons fire spontaneously at rates of 8-10 Hz during the day (Jackson et al. 2004). At night, the activity is suppressed typically to <2 Hz with many cells in the silent state (Inouye and Kawamura 1979; Green and Gillette 1982; Groos and Hendriks 1982; Shibata et al. 1982; Yamazaki et al. 1998). These neurons express a subunit, \( \beta 2 \), having the potential to modify BK channel properties (Montgomery and Meredith 2012; Whitt et al. 2016). The \( \beta 2 \) subunit produces inactivation of BK (Wallner et al. 1999; Xia et al. 1999). Inactivating BK currents are referred to as BK_{i}, BK currents that exhibit relatively little inactivation are referred to as BK_{v}. The primary BK component in the SCN during the day is BK_{i}, whereas BK_{v} is
the primary BK current in the SCN at night (Whitt et al. 2016). The latter group has suggested that the difference in the inactivation properties of these two BK channel types underlies the differences in excitability in SCN neurons between night and day; repetitive firing during the day (BK_d) versus relative quiescence at night (BK_s).

The focus of this report is on the contribution of BK channel current, \( I_{BK} \), to the total current during an action potential (AP) in the daytime. Those results have been measured in SCN neurons using the AP-clamp technique (Jackson et al. 2004; Whitt et al. 2016), a method in which a previously recorded AP is applied to a neuron before and after addition to the external medium of a specific ion channel blocker (Llinas et al. 1982; Bean 2007). For example, the rapidly activating and inactivating sodium ion current, \( I_{Na} \), has been measured in SCN neurons using the AP clamp together with tetrodotoxin, a specific blocker of \( I_{Na} \) (Jackson et al. 2004). The amplitude and time course of \( I_{Na} \) during an SCN AP was determined from the difference between the test and control results of the experiment. Jackson et al. (2004) also reported voltage clamp step recordings of \( I_{Ca} \), the traditional method for analyzing an ionic current (Hodgkin and Huxley 1952). The two approaches together provide a more complete description of a particular ion current component than is provided by voltage clamp step results alone. Jackson et al. (2004) reported a similar analysis for the calcium ion current, \( I_{Ca} \). The \( I_{Ca} \) component is required for BK channel activation during an AP. In a recent study the \( I_{Na} \) and \( I_{Ca} \) results from Jackson et al. (2004) were analyzed computationally to obtain models of these components suitable for SCN neurons (Clay 2015). In this report that analysis has been extended to \( I_{BK} \). The long-term goal of this work is a mathematical model of the AP for SCN neurons.

**Methods**

The results described below require an AP from an SCN neuron, the corresponding AP-clamp measurement of \( I_{BK} \), both of which are provided by Jackson et al. (2004; their Fig 12 with \( I_{BK} \) corresponding to \( I_{K,Ca} \)), and a kinetic model of \( I_{BK} \) gating. The AP and \( I_{BK} \) recordings were digitized (Clay 2015). Those records are shown in Figure 1 with lines connecting the points. Figure 1 also contains simulations of \( I_{BK} \) at various points during the AP. The data sets \( V_i \) vs. \( t_i \) for the AP and \( I_{BK,i} \) vs. \( t_i \) with \( i = 0,1,2,\ldots \), are the basis for the analysis that follows with \( V \) membrane potential in millivolts, time \( t \) in milliseconds, and \( I_{BK} \) in picoamperes. The \( V_i \) vs. \( t_i \) data set for the AP was applied computationally to the model of \( I_{BK} \) given below using Mathematica (Wolfram Research, Champaign, IL; Clay 2015). That model is based on voltage clamp step recordings of Cui et al. (1997) from *mslo*, a clone of the BK channel \( \alpha \) subunit heterologously expressed in *Xenopus* oocytes. Those results were obtained using the inside-out voltage clamp mode so that \( Ca^{2+} \) could be controlled during the experiments. A novel feature of the \( I_{BK} \) model concerns a putative \( Ca^{2+} \) dependence of some of its parameters. The model is given by:

\[
I_{BK}(V, t) = g_{BK} n(V, t)(V - E_K) \tag{1}
\]

where \( g_{BK} \) is BK channel conductance, \( g_{BK} = 38.5 \text{nS} \). \( n(V, t) \) is the voltage- and time-dependent gating variable of the channel, and \( E_K \) is the K⁺ reversal potential, \( E_K = -96 \text{mV} \) (Jackson et al. 2004). The gating variable is determined by:

\[
dn(V, t)/dt = -[z_{BK}(V) + \beta_{BK}(V)]n(t) + z_{BK}(V) \tag{2}
\]

with

\[
z_{BK}(V) = -z_{Ca}(V - V_{Ca})/\{exp[-0.045(V - V_{Ca})] - 1\} \text{msec}^{-1} \tag{3}
\]

\[
\beta_{BK}(V) = \beta_{Ca}\exp[-(V - V_{Ca})/30] \text{msec}^{-1}
\]

The various parameters of the model were determined by comparing its predictions with the recordings of Cui et al. (1997). The model in Equations 1–3 is similar to the one used by Hodgkin and Huxley (1952) for their analysis of \( I_k \) in squid giant axons with a \( Ca^{2+} \) dependence assigned to the model via \( V_{Ca}, z_{Ca}, \) and \( \beta_{Ca} \).
(Equation 3; Results). The $V_t$ vs. $t_i$ data set of the AP in Figure 1 was applied to Equation 2 using a procedure described in Clay (2015) to determine BK channel activation throughout the AP. The start point of the AP in Figure 1 is $t_0 = 0$, $V_o = -58$ mV. This level of $V$ is below activation of $I_{BK}$ during the interspike interval since $Ca^{2+}$ during that time is $\sim 50$ nmol/L, the level of $Ca^{2+}$ in a resting neuron (McCormick and Huguenard 1992). At this level of $Ca^{2+}$, $V = -58$ mV is below the activation range of $I_{BK}$ (Cui et al. 1997; Xia et al. 1999), and so the start value for $n$, $n_0$, is assumed to be 0. The next iterative value of $n$, $n_i$, was determined from Equation 2 with NDSolve (Mathematica), using $V(t) = V_o + (V_f - V_0) (t - t_0) / (t_f - t_0)$ for $t_0 < t < t_f$ ($V_f = -53.5$; $t_f = 5.6$ msec). The iterative values of $Ca^{2+}$ were obtained as described in Clay (2015) and shown below (Results). This procedure was continued throughout the $V_i$ versus $t_i$ data set of the AP waveform. The resulting digitized values of $I_{BK}$ corresponding to Equation 1 are $I_{BK,i} = g_{BK} n_i (V_i - E_{BK})$. Those results are shown in Figure 1 along with the experimental recording of $I_{BK}$. The model for $I_{BK}$ does not contain an inactivation parameter since the results of Cui et al. (1997) do not clearly show inactivation over the duration of the voltage clamp steps - 20 msec - used for those results (Discussion).

**Results**

**Ca$^{2+}$ during an AP**

As noted above, the intracellular calcium ion concentration, $Ca^{2+}$, during an AP from SCN neurons is required to determine $I_{BK}$. A model of $I_{Ca}$ is, in turn, required for this result. This component cannot be described by $I_{Ca} = g_{Ca} (V - E_{Ca})$, where $g_{Ca}$ is $Ca^{2+}$ channel conductance. Rather, $I_{Ca}$ has a nonlinear dependence on the $Ca^{2+}$ driving force (McCormick and Huguenard 1992). That relationship is well described by the Goldman-Hodgkin-Katz (GHK) equation, $I_{Ca} = a (\exp(zq(V - E_{Ca}))/kT-1))/\exp(zqV/kT-1)$, where $a$ is a constant related to $Ca^{2+}$ membrane permeability, $z$ is the ionic valence of a $Ca$ ion, $q = 2$, $q$ is the unit electronic charge, $k$ is the Boltzmann constant and $T$ is the absolute temperature. At room temperature, which was used by Jackson et al. (2004), $kT/2q = 12.5$ mV. The extracellular concentration of $Ca^{2+}$ for the results in Jackson et al. (2004) was 1.2 mmol/L ($Ca^{2+} = 1.2$ mmol/L). The level of $Ca^{2+}$ in neurons is significantly less than 1.2 mmol/L. At rest, $Ca^{2+} = 50$ nmol/L (McCormick and Huguenard 1992). During an AP, $Ca^{2+}$ in the immediate vicinity of BK channels may rise to the 10–20 μmol/L range (Fakler and Adelman 2008), which is also considerably less than 1.2 mmol/L. For the purposes of the GHK equation $Ca^{2+}$ may assumed to be zero without significantly altering the results in this report over the range of potentials spanned by an AP. For $Ca^{2+} = 0$, $I_{Ca} = - aGHK(V)$ with $GHK(V) = (V/12.5)/\exp(V/12.5)-1$. Note that $GHK(V = 0) = 1$. For the purposes of BK channel activity as well as other features of SCN neuron behavior, $Ca^{2+}$ is, of course, not zero. In particular, $Ca^{2+}$ undoubtedly has “hot spots” adjacent to the Ca/BK complexes within the membrane during an AP (Fakler and Adelman 2008). This distribution has been simplified for modeling purposes by the assumption of two intracellular compartments for $Ca^{2+}$ (Yamada et al. 1998; Diekman et al. 2013). One compartment corresponds to a thin spherical shell 0.1 μmol/L in thickness near the membrane surface (McCormick and Huguenard 1992). The $Ca^{2+}$ concentration in this compartment is denoted by $Ca_s$. The other compartment corresponds to the cytosol. The $Ca_s$ parameter is given by:

$$\frac{dCa_s}{dt} = -K_1I_{Ca} - K_2Ca_s + c_i \tag{4}$$

with $K_1 = 3 \times 10^{-5}$ M/nC, $K_2 = 0.04$ ms$^{-1}$ (Purvis and Butera 2005), $c_i = 2$ mmol/L/ms, and

$$I_{Ca_s}(V, t) = -GHK(V)f(t)[305r_1^2(V, t) + 31r_2(V, t)] \tag{5}$$

where $f(t)$ is $I_{Ca_s}$ inactivation, and $r_1$ and $r_2$ are the gating activation parameters for the two types of $I_{Ca}$ channels present in SCN neurons, one of which appears to be the L-type channel based on its sensitivity to nimodipine. The other component is nimodipine-insensitive (Jackson et al. 2004). A full description of the $I_{Ca}$ model is given in Clay (2015). The model was previously applied to the AP in the inset of Figure 5B of Jackson et al. (2004) - Fig 8 of Clay (2015) - used for their AP-clamp recording of $I_{Ca_s}$. A similar analysis was carried out here (Fig. 2, bottom panel) for the AP illustrated in Figures 1 and 2 which, as
noted above, corresponds to the AP used by Jackson et al. (2004) for their AP-clamp recording of $I_{BK}$. The $I_{Ca}$ analysis must necessarily be carried out for the same AP used for the AP-clamp recording of $I_{BK}$.

$I_{BK}$ model

The model for $I_{BK}$, Equations 1–3, predicts a response to a rectangular voltage clamp step that is consistent with a single exponential function of time, as in the results of Cui et al. (1997). Similar results have been reported for BK splice variants heterologously expressed in HEK cells (Shelley et al. 2013), as well as results from msl0/CaV channel complexes also heterogously expressed in HEK cells (Cox 2014). As noted above, the $Ca_{2+}$ dependence of the model is contained in the $V_{Ca}$, $c_{Ca}$, and $b_{Ca}$ parameters. Specifically, $V_{Ca} = 147–75 \log(Ca_{s}/Ca_{o})$ mV with $Ca_{o} = 1 \mu mol/L$, $c_{Ca} = 0.03/[1 + (\log(Ca_{s}/Ca_{o}))^2]$, and $b_{Ca} = 0.04/[1 + (\log(Ca_{s}/Ca_{o}))^2]$. The predictions of the model for voltage steps from 20 to 110 mV in 10 mV increments with $Ca_{s} = 10.2 \mu mol/L$ are shown in the left-hand panel of Figure 3. These results are to be compared with the corresponding experimental recordings in Figure 1A of Cui et al. (1997). The deactivation kinetics in the right-hand panel of Figure 3 are to be compared with the corresponding results in Figure 1B of Cui et al. (1997).

$Ca_{2+}$ dependence of $I_{BK}$ results

Cui et al. (1997) reported results for $Ca_{s}^{2+} = 0.84, 1.7, 4.6, and 10.2 \mu mol/L$, as well as higher levels of $Ca_{s}^{2+}$. The channel activation curves for $0.84 \leq Ca_{s}^{2+} \leq 10.2 \mu mol/L$, given in their Figure 5B, are reproduced here in Figure 4. These results represent currents at the end of 20 msec duration voltage steps, sufficiently long so that the channel kinetics at any given voltage were at their steady-state level. In the model these results correspond to $n_{\infty} = \frac{1}{a_{BK}(V_{s},V_{Ca})/(V_{s}^{3})/\beta_{BK}(V_{s},V_{Ca})}$ with $a_{BK}$ and $\beta_{BK}$ as given by Equation 3. The predictions of this equation for $n_{\infty}$ are represented by the curves in Figure 4. The time constants of the model, $\tau_{BK}$, are given by $\tau_{BK} = 1/(a_{BK}+\beta_{BK})$. This equation predicts the bell-shaped curves in Figure 5 shown along with experimental results for $\tau_{BK}$ from Cui et al. (1997) corresponding to $Ca_{s}^{2+} = 0.84, 1.7, and 10.2 \mu mol/L$. The curve for $Ca_{s} = 0.84 \mu mol/L$ is shifted leftward on the voltage axis by an increase in $Ca_{s}$, similar to the results for the activation curves (Figure 4). The maximal time constant at any given level of $Ca_{s}$ is itself dependent upon $Ca_{s}$ a bell-shaped dependence as indicated in Figure 1D of Cox (2014). Results for $\tau_{BK}$ from Cui et al. (1997) and Cox (2014) normalized by the maximum time constant for $Ca_{s}^{2+} = 0.9 \mu mol/L$ in the Cox (2014) report are shown in Figure 6 along with the corresponding prediction of the model, $1/(1 + (\log(Ca_{s}/Ca_{o}))^2)$. Cox (2014) reported results for $Ca_{s}^{2+} = 0.003 \mu mol/L$ and 118 $\mu mol/L$ (neither of which is shown in Figure 6). The former is below the resting level of $Ca_{s}^{2+}$, which is 0.05 $\mu mol/L$. (McCormick and Huguenard 1992). The latter, $Ca_{s}^{2+} = 118 \mu mol/L$, would appear to be well above the maximum level of $Ca_{s}^{2+}$ reached during an AP (10–20 $\mu mol/L$, Berkenfeld et al. 2006; Fakler and Adelman 2008). Cox (2014) described a detailed model of BK channel activation including the effects of $Ca_{s}^{2+}$ on activation gating. The model in this report is relatively simple, which is useful for the analysis of $I_{BK}$ during an AP. Those results are qualitatively similar to the experimental recording of $I_{BK}$, although their timing does not completely match experiment. The simulations assume that the effect of a change in $Ca_{s}$ on BK channel kinetics is not affected by changes in other factors such as voltage, pH, or temperature.

![Figure 3](image-url)  
**Figure 3.** Predictions of the model in Equations 1–3 for $I_{BK}$. Left panel: Currents elicited from the model with 6 msec duration voltage clamp steps from -20 to +110 mV, with 10 mV increments between each step. Initial value of $n(t)$ at the beginning of each step was $n = 0$. Right panel: Deactivation currents for an initial value of $n = 1$ with $V = -10, -30, -50,$ and $-70$ mV.

![Figure 4](image-url)  
**Figure 4.** Relative conductance for $I_{BK}$ as a function of $Ca_{s}$. The data points with error bars were taken from Figure 5B from Cui et al. (1997). The curves correspond to $n_{\infty} = \frac{1}{a_{BK}(V_{s},V_{Ca})/(V_{s}^{3})/\beta_{BK}(V_{s},V_{Ca})}$ with $a_{BK}$ and $\beta_{BK}$ given in Equation 3 and $c_{Ca} = 0.03/[1 + (\log(Ca_{s}/Ca_{o}))^2]$, $b_{Ca} = 0.04/[1 + (\log(Ca_{s}/Ca_{o}))^2]$, and $V_{Ca} = 147–75 \log(Ca_{s}/Ca_{o})$ mV.
channel kinetics occurs instantaneously. Alternatively, a delay of a few milliseconds may be involved (Hille 2001; Martinez-Espinosa et al. 2014), which could account for the difference between experiment and theory in Figure 1.

**Discussion**

As noted above (Introduction), Whitt et al. (2016) have suggested that BK channel inactivation is a significant factor in SCN excitability. Specifically, BK<sub>i</sub>, the primary BK channel component during the day, exhibits pronounced inactivation during voltage clamp step recordings, whereas BK<sub>s</sub>, the primary BK component at night, does not. However, significant inactivation of BK occurs only for \( V > +30 \text{ mV} \) (Whitt et al. 2016; Fig. 2a), which is above the maximum overshoot potential of the SCN AP (Jackson et al. 2004; Fig. 2). Moreover, the time constant of inactivation at potentials for which it does occurs is ~45 msec, and that result is relatively insensitive to changes in \( V \) (Whitt et al. 2016). The duration of the SCN AP at its midpoint is ~4 msec (Jackson et al. 2004), significantly less than the time constant of inactivation. The membrane potential spends considerably less time than 4 msec at potentials greater than 0 mV. These observations taken together suggest that BK inactivation is not an important factor for excitability in the SCN. Another aspect of BK channel gating, its activation curve, could be significant. The \( \beta_2 \) subunit not only produces inactivation of BK at strongly depolarized potentials, it also shifts the BK channel activation curve leftward on the voltage axis for a given level of Cai<sup>2+</sup> (Wallner et al. 1999; Xia et al. 1999). Results from BK<sub>i</sub> and BK<sub>s</sub> channels in rat adrenal chromaffin cells (RCC) may be relevant to the roles of these channels in the SCN. The activation curve for BK<sub>i</sub> in those cells is also shifted leftward relative to the activation curve for BK<sub>s</sub> (Sun et al. 2009). Constant current injection in a model of an RCC with BK<sub>i</sub> produces repetitive firing, whereas constant current injection in model cell having BK<sub>s</sub> produces only one or a very few APs (Sun et al. 2009). As noted by Sun et al. (2009), “...These differences arise, not because of the inactivation behavior of BK<sub>i</sub> current, but from the more negatively shifted range of activation of BK<sub>i</sub> channels at a given Cai<sup>2+</sup> in comparison to BK<sub>s</sub> current.” A similar conclusion may apply to the SCN. Specifically, the diurnal changes that occur in the SCN may be attributable to a voltage shift of the BK channel activation curve produced by the \( \beta_2 \) subunit rather than inactivation of the BK channel which, additionally, appears to occur outside of the range of membrane potentials spanned by an AP. The results in this report are based on a clone of the \( \alpha \) subunit, a BK channel which does not possess the \( \beta_2 \) subunit. A leftward shift of the activation curve attributable to that subunit may produce an increase in the difference between experiment and theory in Figure 1, a delay in the onset of the
effects of a change in $C_{ai}$ on BK channel gating that is greater than the delay indicated in Figure 1. Additional experiments and simulations of $I_{BK}$ during an AP may be needed to clarify this issue.

The effects of $C_{ai}^{2+}$ on BK channels are similar, in some respects, to the effects of $C_{ai}^{2+}$ on synaptic vesicle release in nerve terminals following an AP (Neher 1998; Augustine et al. 2003). An AP triggers entry of $C_{ai}^{2+}$ into the terminal via voltage-gated $C_{ai}^{2+}$ channels. These channels almost certainly lie in close proximity to vesicle release sites. As a result, the local $C_{ai}^{2+}$ concentration may briefly rise to levels of 100 μmol/L, or higher (Neher 1998). BK channel activation in presynaptic nerve terminals has been used to report these levels of $C_{ai}^{2+}$ (Yazejian et al. 2000). Following an AP, vesicle release drops precipitously, which is consistent with a requirement for channel activation with very low $C_{ai}^{2+}$, probably due to various $C_{ai}^{2+}$ buffering mechanisms (Parnas and Parnas 1994; Neher 1998). In SCN neurons $C_{ai}^{2+}$ channels are likely to be in close proximity to BK channels similar to the relationship between $C_{ai}^{2+}$ channels and vesicle release sites in presynaptic nerve terminals. During an AP, the $C_{ai}^{2+}$ concentration in the vicinity of BK channels may rise to somewhere in the 10–20 μmol/L range, or perhaps higher (Berkenfeld et al. 2006; Fakler and Adelman 2008). The simulation in Figure 2 is consistent with this result. Specifically, $C_{ai}$ equals 15 μmol/L midway through repolarization of the AP. Calcium ion buffers may not be required to reduce this level of $C_{ai}^{2+}$ thereby terminating BK channel activation because repolarization of the AP, a process to which $I_{BK}$ contributes, brings the membrane potential below BK channel threshold even with $C_{ai}$ in the 1–10 μmol/L range. In this sense $I_{BK}$ is self-limiting. The time between APs in a spontaneously firing SCN neuron during the day is approximately 100 msec, considerably longer at night, either of which is sufficient for $C_{ai}^{2+}$ to diffuse passively away from the membrane bringing $C_{ai}$ to its baseline level prior to the subsequent AP. Indeed, $C_{ai}$ in the simulation in Figure 2 is reduced below 15 μmol/L by passive diffusion even before the AP has ended.

Voltage-dependent activation of BK channels may not require the presence of $C_{ai}^{2+}$, although strong depolarizations are needed for channel activation with very low $C_{ai}^{2+}$. For example, Cui et al. (1997) reported mslo channel currents with $C_{ai}^{2+} = 0.5$ nmol/L. Cox (2014) reported similar results with $C_{ai}^{2+} = 3$ nmol/L. The midpoint of the channel activation curve for these conditions is $V = +200$ mV for $C_{ai}^{2+} = 0.5$ nmol/L and $V = +150$ mV for $C_{ai}^{2+} = 3$ nmol/L, both of which are well positive to the range of potentials spanned by an AP even with a 50-60 mV leftward shift of the activation curve on the voltage axis caused by the β2 subunit (Xia et al. 1999).

As noted above, this work may have significant implications for computational models of the AP for neurons in which BK channels are present. In traditional models, such as the Hodgkin and Huxley (1952) model of the AP in squid giant axons, the intracellular and extracellular concentrations of permeant ions, Na$^+$ and K$^+$ in the case of squid axons, are fixed throughout the AP although the effective extracellular K$^+$ concentration can change due to K$^+$ accumulation in the extracellular space between the axolemma and the surrounding Schwann cell (Frankenhauser and Hodgkin 1956). This effect can be accounted for in the AP model by assigning a time dependence to $E_K$ (Clay 1998). The intracellular $C_{ai}^{2+}$ concentration provides another example of an ion concentration not remaining fixed during an AP, especially in the vicinity of BK channels. This result does not significantly change the driving force, $V-E_{Ca}$, over the range of potentials spanned by the AP (Clay 2015). The intracellular $C_{ai}^{2+}$ concentration, $C_{ai}^{2+}$, does not appear in the expression given above for GHK($V$) - RESULTS. A change in $C_{ai}^{2+}$ does modify BK kinetics, perhaps with a delay and that delay would have to be accounted for in a model of the AP.

**Conflict of Interest**

No conflict of interest, financial or otherwise, are declared by the author.

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