Lipid is heterogeneously distributed in muscle and associates with low radiodensity in cancer patients

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Abstract

Background Low muscle radiodensity is associated with mortality in a variety of cancer types. Biochemical and morphological correlates are unknown. We aimed to evaluate triglyceride (TG) content and location as a function of computed tomography (CT)-derived measures of skeletal muscle radiodensity in cancer patients.

Methods Rectus abdominis (RA) biopsies were collected during cancer surgery from 75 patients diagnosed with cancer. Thin-layer chromatography and gas chromatography were used for quantification of TG content of the muscle. Axial CT images of lumbar vertebra were used to measure muscle radiodensity. Oil Red O staining was used to determine the location of neutral lipids in frozen muscle sections.

Results There was wide variation in RA radiodensity in repeated measures (CV% ranged from 3 to 55% based on 10 serial images) as well as within one slice (CV% ranged from 6 to 61% based on 10 subregions). RA radiodensity and total lumbar muscle radiodensity were inversely associated with TG content of RA (r = −0.396, P < 0.001, and r = −0.355, P = 0.002, respectively). Of the total percentage area of muscle staining positive for neutral lipid, 54 ± 17% was present as extramyocellular lipids (range 23.5–77.8%) and 46 ± 17% (range 22.2–76.5%) present as intramyocellular lipid droplets.

Conclusions Repeated measures revealed wide variation in radiodensity of RA muscle, both vertically and horizontally. Low muscle radiodensity reflects high level of TG in patients with cancer. Non-uniform distribution of intramyocellular and extramyocellular lipids was evident using light microscopy. These results warrant investigation of mechanisms resulting in lipid deposition in muscles of cancer patients.

Keywords Fat infiltration; Hounsfield units; Muscle attenuation; Myosteatosis; Rectus abdominis; Skeletal muscle

Introduction

Computed tomography (CT) imaging has recently revealed that a reduced level of muscle radiodensity is associated with shorter survival and systemic inflammation in cancer patients.¹⁻⁶ Radiodensity is measured in Hounsfield units (HU), which is a linear transformation of the attenuation coefficient, where the radiodensity of distilled water at standard pressure and temperature is defined as 0 HU and the radiodensity of air at standard temperature and pressure is defined as −1000 HU.⁷,⁸ Reduced muscle radiodensity has also been associated with insulin resistance,⁹,¹⁰ mitochondrial dysfunction,¹¹ decrease in contractile force of the muscle,¹² low aerobic capacity,⁹ and impaired lipolytic response.¹³
The presence of abnormal levels of lipid in skeletal muscle has been associated with aging, frailty, chronic back pain, diabetes, obesity, chronic obstructive pulmonary disease, and cancer. Lipid content has been reported in various muscle groups, including the quadratus lumborum, vastus lateralis, and mid-thigh, and is noted for its non-uniform distribution across the length of a muscle. Even in healthy muscle, lipid deposits are clustered in certain areas, notably in the vascularized areas of the intermuscular connective tissue. On this basis, it was expected that lipids would not be uniformly distributed within the muscles of cancer patients and that there would be variation in muscle radiodensity within the same muscle group.

Based on a study by Goodpaster et al., in which the relationship of mid-thigh muscle radiodensity and triglyceride (TG) content in healthy and diabetic patients was reported, it has been assumed that low muscle radiodensity is related to high TG content of rectus abdominis (RA). However, this relationship between radiodensity and TG content must be re-examined in cancer patients for a number of reasons. First, body composition studies in cancer patients are typically performed using CT images acquired in the lumbar region axial images at the third lumbar vertebra (L3). The physicochemical properties of lumbar muscles may differ substantially from muscles of the limb. Second, in the report from Goodpaster and coworkers, muscle radiodensity was reported as mean radiodensity from all pixels within the range of 0–100 HU at mid-thigh cross section, whereas in the oncology setting, standardized measures of muscle between −29 and 150 HU are widely applied.

Skeletal muscles contain lipid deposits found deep in the fascia and within muscles, referred to as extramyocellular lipid (EMCL) as well as lipid droplets inside muscle fibres, referred to as intramyocellular lipid (IMCL). IMCL is associated with insulin resistance, inflammation, and functional deficit in skeletal muscle. EMCL can originate from adipogenic differentiation of stem cell populations of skeletal muscle. In cancer patients, it is not known whether lipids are located inside muscle fibres as IMCL or adjacent to the muscle fibres within adipocytes as EMCL. The aetiology of each lipid depot is different; therefore, characterization of location of lipid deposition in muscles is important.

A number of studies have used RA biopsies in cancer patients to delineate biological features associated with low muscle mass and radiodensity. The primary aim of this study was to gain an appreciation of the variation in muscle radiodensity within the RA. Our collateral aim was to investigate the association between the clinically derived measure of muscle radiodensity and TG content in the RA of cancer patients. Finally, we sought to understand how lipid content was distributed in the intramyocellular and extramyocellular compartments.

**Materials and methods**

**Ethics statement**

The study was approved by the Health Research Ethics Board of Alberta—Cancer Committee. Patients undergoing elective abdominal surgery were consecutively approached to participate in tumour and tissue banking at a hepatopancreatobiliary surgical service in Alberta, Canada. Muscle biopsies were obtained from the University of Calgary Hepatopancreaticobiliary/Gastrointestinal Tumor Bank. Three per cent of approached patients declined participation. Patients provided written informed consent for muscle biopsy and tissue banking. Release of 75 samples from the bank for analysis, as well as patient information (demographic, clinical, and operative data) from medical records, was performed under the auspices of Protocol ETH-21709: The Molecular Profile of Cancer Cachexia.

**Subjects and muscle biopsies**

The study cohort and conditions for acquisition of muscle samples have been described previously. Briefly, RA biopsies (0.5–3 g) were collected from cancer patients (>18 years old) undergoing open abdominal surgery scheduled as part of their clinical care. Biopsies were collected at the start of surgery using sharp dissection and without the use of electrocautery. Samples were processed under sterile conditions. Visible adipose and connective tissues were trimmed. One piece of biopsy was immediately frozen in liquid nitrogen and stored at −80°C. Another piece was frozen in isopentane cooled at −160°C in liquid nitrogen and stored at −80°C for cryostat sectioning and Oil Red O (ORO) staining and morphological analysis. Diagnosis was confirmed before including patients in current study. Age and cancer type were abstracted from medical charts.

**Computed tomography image analysis**

Pre-operative CT scans completed with a spiral CT scanner for initial cancer staging and surgical planning were used to quantify skeletal muscle area and radiodensity. Images were analysed using SliceOmatic® V4.2 software with CT image parameters that include contrast, 5 mm slice thickness, 120 kVP, and 290 mA. Total skeletal muscle area (cm²) was evaluated on an axial single image at L3 using Hounsfield unit (HU) thresholds of −29 to 150 for skeletal muscle. The sum of skeletal cross-sectional muscle areas was normalized for stature (m²) and reported as skeletal muscle index (cm²/m²). Muscle radiodensity was assessed as the mean value for the full range of −29 to +150 HU. Mean lumbar muscle radiodensity is reported for the entire muscle area (quadratus...
lumborum, psoas, erector spinae, external obliques, transverse abdominis, internal obliques, and RA) and RA alone within the L3 image. Mean time period between CT image and biopsy collection was 35 ± 59 days. To examine the variation in muscle radiodensity within RA, a series of 10 vertical slices at 5 mm intervals from each other were analysed for all patients. To examine the variation within same slice of RA, muscle radiodensity was measured at 10 different regions of interest in the single-image slice in 13 patients. Ten different regions of interest were selected in the single-image slice. The area near the boundary of the muscles was avoided to ensure that subcutaneous, visceral adipose, tissue and intramuscular fat area were excluded.

**Triglyceride content of rectus abdominis**

Triglyceride content of each muscle biopsy was analysed in duplicate. Biopsy (≥50 mg) was ground using a frozen pestle and mortar without letting the muscle tissue thaw. Ground tissue was homogenized in 1.6 mL of calcium chloride (CaCl₂; 0.025%) solution with glass beads (0.5 mm diameter; FastPrep®-24, MP Biomedicals, Santa Ana, CA, USA) in 20 s intervals for 1 min total. Samples were placed on ice for at least 15 s between each homogenization interval. A modified Folch method was used to extract lipids using chloroform/methanol (2:1, v/v) as previously described. The TG fraction was isolated on G-plates, and the TG band was identified and scraped from G-plates. An internal standard C15:0 (10.2 mg per 100 mL of hexane) was added, followed by saponification and methylation. Fatty acid composition was determined using gas chromatography–flame ionization detector analysis on a Varian 3900 (Varian Instruments, Georgetown, ON, Canada). Fatty acids were separated between 6 and 24 carbon chain lengths and identified using a fatty acid standard of known composition (GLC-82 and GLC-502, Nu-Chek-Prep, USA). Quantity of fatty acids within the TG fractions was calculated by comparison with the known concentration of the internal standard, and sum of all fatty acids was reported as total TG. The coefficient of variance was <5%.

**Immunofluorescence: Oil Red O**

Tissues were cryosectioned transversely (10 μm thick) and stained for neutral lipid content using ORO as previously described. Primary and secondary antibodies are described in the supplementary materials (Supporting Information, Table S2). Laminin staining and dystrophin staining were used to define muscle cell membranes, aiding in lipid location. Briefly, sections were fixed with 10% formalin, followed by incubation with primary antibodies, laminin (1:200) and dystrophin (1:25), and secondary antibody, Alexa Fluor 488. Sections were immersed in ORO for 30 min at room temperature. Muscle sections were visualized with a spinning disk confocal microscope (Quorum Wave FX Spinning Disc Confocal System, Quorum Technologies). An Electron-Multiplying Charge-Coupled Device cooled camera (Hamamatsu; Quorum Technologies, Guelph, 80 ON, Canada) and Volocity 6.3 software (PerkinElmer, Waltham, MA, USA) were used to capture and analyse all images. Visualization and quantification were performed as previously described. Z-stacked images captured tissue sections using a 20×/0.85 oil lens and were assembled together and plane merged to create a composite image that enabled the visualization of a whole and clear tissue cross section. A software script was established to identify muscle fibres using intensity of the laminin/dystrophin stain. Neutral lipids were quantified by establishing thresholds for the intensity of ORO staining and calculating the number of red pixels in relation to μm² of the section analysed. Once thresholds were set, quantitation then proceeded by Volocity software. The total area stained with ORO was reported as a percentage of the total area of tissue analysed. Intramyocellular and extramyocellular lipids were defined based on whether ORO stain was present inside or outside muscle fibre boundaries delimited by laminin/dystrophin staining.

**Immunofluorescence: fibre types**

Muscle serial sections (10 μm) were cryosectioned (cryostat Leica model CM300) transversely at −22°C and stored at −80°C until staining. Myosin heavy chain (MyHC) I, IID, and IIA were determined as previously described. Primary and secondary antibodies are described in Supporting Information, Table S2. After the secondary antibody application, a nuclear stain (4′,6-diamidino-2-phenylindole, DAPI) was added for 2 min and washed. Slides (Apex™ superior adhesive slides, Leica Biosystems) were mounted, covered, and let dry for 12 h. Images for tissue sections were acquired using a 20×/0.85 oil lens with a spinning disk confocal microscope (Quorum Wave FX Spinning Disc Confocal System, Quorum technologies). Individual Z-stacked images were assembled to create a composite image of a whole-tissue cross section. Tissue images were captured and analysed with Volocity 6.3 software (PerkinElmer). A software script was established to identify muscle fibre types (I, I/IIA, IIA, IIA/D, and D) using intensity of the MyHC stains and quantified automatically by the software.

**Statistical analysis**

Descriptive statistics were reported as mean ± standard deviation. Categorical data were presented as counts with percentages. Shapiro–Wilk test was used to test for normality. TG data were not normally distributed, so non-parametric tests were used for analysis. Comparisons between groups...
were conducted using Mann–Whitney U test and χ² test for categorical variables. For the association between TG content of RA and muscle radiodensity, Spearman’s rho (non-parametric test) was used because TG content data were not normally distributed. Least significant change was determined by international standards as set by the International Society for Clinical Densitometry. Statistical significance was reported when P-value < 0.05. Correlation coefficients are referred to as high (>0.5), moderate (0.3–0.5), and low (<0.3). All statistical analyses were performed using IBM SPSS® software, Version 20 (Chicago, IL, USA) for Windows.

Results

Patient characteristics

Patient characteristics are shown in Table 1. The study population consisted of 58 (77%) male patients and 17 (23%) female patients with a mean age of 63.2 ± 10.9 years and mean body mass index of 25.0 ± 10.6 kg/m². There was significant difference in mean skeletal muscle index, muscle radiodensity, cross-sectional area of subcutaneous adipose tissue, and TG content of RA between male and female patients (Table 1). Colorectal cancer was the most common cancer type, comprising 44% of the population followed by pancreatic cancer (29%). Almost a quarter of the patients had metastatic disease. Hypertension (37%) was the most common co-morbidity followed by diabetes (17%) and cardiovascular disease (17%).

Variation in muscle radiodensity within rectus abdominis

Analysis of RA at 10 slices and 10 regions is illustrated in Figure 1A and 1B. The variation in RA radiodensity within 10 distinct slices at 5 mm interval is illustrated in Figure 2A. The narrowest within-subject range of RA radiodensity in 10 slices was 4 HU, and the highest was 18 HU (CV% ranged from 3 to 55% based on 10 serial images). The variation in RA radiodensity within 10 regions of interest in the same CT image slice of 13 patients is illustrated in Figure 2B. The least significant change was calculated for 10 slices and was found to be 8.65 HU. The narrowest within-subject range of RA radiodensity in 10 regions of interest was 10 HU, and the highest was 70 HU (CV% ranged from 6 to 61% based on 10 subregions).

Triglyceride content of muscle was associated with rectus abdominis and total muscle radiodensity at the third lumbar vertebra

Radiodensity of RA at L3, total lumbar muscle radiodensity at L3, and TG content of RA biopsy were analysed for 75 patients. Radiodensity of RA at L3 ranged from −10.8 to 50.6 HU, total lumbar muscle radiodensity at L3 ranged from

Table 1: Characteristics of patients with cancer

| Characteristic                          | Male (n = 58) | Female (n = 17) | All patients (n = 75) | P-value |
|----------------------------------------|--------------|----------------|----------------------|---------|
| Age (years), mean ± SD                 | 62.6 ± 11.4  | 66.2 ± 7.0     | 63.2 ± 10.9          | NS      |
| Tumour type, N (%)                     |              |                |                      |         |
| Colorectal                             | 26(45)       | 7(41)          | 33(44)               | NS      |
| Pancreatic                             | 18(31)       | 4(31)          | 22(29)               | NS      |
| Other gastrointestinalb                 | 15(25)       | 5(29)          | 20(27)               | NS      |
| Presence of metastasis, N (%)          | 12(20)       | 8(47)          | 20(26)               | NS      |
| BMIb (kg/m²), mean ± SD                | 24.9 ± 10.1  | 25.4 ± 12.7    | 25.0 ± 10.6          | NS      |
| CT image measures at L3                 |              |                |                      |         |
| Skeletal muscle index (cm²/m²)          | 49.4 ± 8.1   | 41.0 ± 6.3     | 47.9 ± 8.7           | 0.001   |
| Muscle radiodensity (HU)                | 33.2 ± 9.3   | 26.7 ± 8.3     | 31.9 ± 9.3           | 0.009   |
| Subcutaneous adipose tissue (cm²)       | 186.7 ± 102.2| 308.8 ± 176.6  | 205.9 ± 131.3        | 0.003   |
| Visceral adipose tissue (cm²)           | 196.7 ± 92.6 | 165.5 ± 70.1   | 173.6 ± 96.1         | NS      |
| Co-morbidities, N (%)                   |              |                |                      |         |
| Diabetes type II                        | 9(13)        | 4(24)          | 13(17)               | NS      |
| Hypertension                            | 20(29)       | 8(47)          | 28(37)               | NS      |
| Cardiovascular disease                  | 12(18)       | 1(6)           | 13(17)               | NS      |
| Dyslipidaemia                           | 9(15)        | 4(24)          | 13(17)               | NS      |
| Smoking habit, N (%)                    | 8(14)        | 3(18)          | 11(15)               | NS      |

BMI, body mass index; SD, standard deviation. Values are mean ± SD, except for categorical variable, where numbers in each category are shown. Skeletal muscle index was measured by normalizing cross-sectional muscle area for height, and muscle radiodensity was measured as the average Hounsfield units (HU) of the total skeletal muscle area on a single cross-sectional computed tomography (CT) image at the level of the third lumbar vertebra (L3).
bSmall bowel, bile duct, liver, appendix, stomach, and gall bladder.

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7.1 to 54.4 HU, and TG content of RA ranged from 0.7 to 88.7 μg/mg.

Rectus abdominis radiodensity was moderately negatively associated with TG content of the muscle \( r = -0.396, P < 0.001 (N = 75) \) (Figure 3A). Similarly, there was a moderate negative association between TG content and total lumbar muscle radiodensity \( r = -0.355, P = 0.002 (N = 75) \) (Figure 3B). These results suggest that both mean muscle radiodensity at L3 and RA are associated with TG content of the muscle in cancer patients. An association between TG content and percentage area of ORO was observed \( r = 0.62, P = 0.002 \). No significant association was found between percentage ORO area in the muscle section and muscle radiodensity \( r = -0.24, P = 0.31 \).

**Location of neutral lipid in rectus abdominis muscle**

A variable pattern of neutral lipids was observed in the muscle sections by the use of ORO staining (Figure 4). Fibres with
>50% of total area stained with neutral lipids were observed (Figure 4A). While this was generally uniformly distributed across each fibre, some regions showed focal deposition of lipid droplets near cell membrane (Figure 4B). Perivascular deposition of adipocytes was also exhibited in muscle sections (Figure 4C).

Total area stained for neutral lipids in muscle section was on average 13% (4 to 30%). Out of the total lipid area, mean proportion of IMCL and EMCL areas were 46 and 54%, respectively. Even though almost equal proportions of IMCL and EMCL overall were observed, the ranges of percentage area were wide. IMCL area ranged from 22 to 76%; likewise, EMCL area range from 24 to 78% (Figure 5), and this was not associated with radiodensity measures and TG content of the muscle. Figure 6 illustrates variation in IMCL and EMCL in muscle sections of four cancer patients. Subjects 1 and 2 with similar percentage of neutral lipid area and TG content of RA showed variation in lipid distribution pattern. Subject 1 had higher IMCL (62%) and lower EMCL (38%), and Subject 2 had a similar percentage of IMCL and EMCL, 56 and 44%,
Computed tomography imaging is commonly used by our research group and others to investigate associations between muscle radiodensity and clinical outcomes in cancer patients. Low muscle radiodensity in people with cancer is assumed to reflect lipid infiltration. This is the first study to report variation in RA radiodensity within the same slice of CT image and also across the length of RA. We also found an association between RA/total lumbar radiodensity at L3 and TG content of biopsies in cancer patients. Furthermore, neutral lipid staining revealed heterogeneous distribution of IMCL and EMCL.

The purpose of this study was to assess the variability of radiodensity within RA. Analysis of radiodensity across the length and breadth of RA revealed wide variation within the same subject confirming non-uniform distribution of lipids in the muscle. Generally, research studies in oncology settings followed the lead of Shen et al. to use a single CT image at L3 as muscle area at this level strongly correlates with whole-body volume of muscle. Muscle radiodensity is also measured at L3, but it does not represent spatial pattern and volume distribution of lipid in the whole muscle.

An increasing number of investigators are collecting RA biopsies to study biological features of muscles of cancer patients. In practice, RA biopsies collected during surgery will vary depending on the site of incision. Thus, the biopsy is possibly from a different area of the abdomen than the area of muscle radiodensity evaluation. Also, the biopsy is small relative to the area being evaluated for radiodensity, and the pattern of lipid deposition is heterogeneous. Collectively, these sources of variation explain the moderate correlation between RA radiodensity at L3 or total lumbar muscle radiodensity at L3 and TG content of the biopsy in our study. This also explains why there was no significant correlation between neutral lipid content measured by ORO staining and muscle radiodensity, in contrast to Goodpaster et al.

**Figure 3** Association between muscle radiodensity and triglyceride (TG) content of rectus abdominis (RA). (A) Association between mean RA radiodensity at the third lumbar (L3) region and total TG content, \( r = -0.396, P < 0.001 (N = 75) \). Muscle radiodensity of RA was determined at L3 slice of computed tomography (CT) images obtained from medical records of the patients. (B) Association between total mean lumbar muscle radiodensity at L3 and total TG content measured in RA biopsy, \( r = -0.355, P = 0.002 (N = 75) \). Total muscle radiodensity was analysed at L3 slice of CT images. TG content was analysed by biochemical extraction followed by quantitative gas chromatography. Spearman’s rho analysis was used to determine the associations. In male patients, correlation between TG content of RA and muscle radiodensity of RA or at L3 was weak but significant, \( r = -0.230, P < 0.048 \), and \( r = -0.285, P < 0.030 \), respectively. Similarly, in female patients, weak significant association was observed between TG content of RA and total muscle radiodensity at L3 \( (r = -0.201, P < 0.04) \), but strong significant association was observed between TG content and muscle radiodensity of RA \( (r = -0.581, P < 0.014) \).

|                | Mean       | Range      |
|----------------|------------|------------|
| TG content of RA | 17 \( \mu \)g/mg | 0.7 to 88.7 \( \mu \)g/mg |
| RA muscle radiodensity at L3 | 24 HU | -11 to 51 HU |
| Total muscle radiodensity at L3 | 52 HU | 7.1 to 54.4 HU |

**Discussion**

Computed tomography imaging is commonly used by our research group and others to investigate associations between muscle radiodensity and clinical outcomes in cancer patients. Low muscle radiodensity in people with cancer is assumed to reflect lipid infiltration. This is the first study to report variation in RA radiodensity within the same slice of CT image and also across the length of RA. We also found an association between RA/total lumbar radiodensity at L3 and TG content of biopsies in cancer patients. Furthermore, neutral lipid staining revealed heterogeneous distribution of IMCL and EMCL.
A Variation in neutral lipids in muscle fibres.

Neutral lipid area in the muscle fiber = 23%

Neutral lipid area in the muscle fiber = 43%

Neutral lipid area in the muscle fiber = 56%

B Neutral lipids near cell membrane

With laminin and ORO

ORO only

C Adipocytes in muscle

Adipocytes in the perivascular area of the muscle. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and ORO (bright red) for neutral lipids. Scale bars, 45 μm. (B) Lipid droplets in the area near the cell membrane. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and ORO (bright red) for neutral lipids. Zoomed images show deposition of lipid droplets in the area around the cell membrane. Scale bars, 45 μm. (C) Adipocytes in the perivascular area of the muscle. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and ORO (bright red) for neutral lipids. Scale bars, 140 μm.

Figure 4 Neutral lipid staining revealed different lipid distribution patterns in muscle fibres of cancer patients. (A) Variation in lipid deposition inside muscle fibre. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and Oil Red O (ORO) (bright red) for neutral lipids. Zoomed images show variation in per cent area of neutral lipids within fibres. Scale bars, 45 μm. (B) Lipid droplets in the area near the cell membrane. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and ORO (bright red) for neutral lipids. Zoomed images show deposition of lipid droplets in the area around the cell membrane. Scale bars, 45 μm. (C) Adipocytes in the perivascular area of the muscle. (i) and (ii) are muscle sections of two patients stained with laminin and dystrophin (green) for cell membrane and ORO (bright red) for neutral lipids. Scale bars, 140 μm.
recent study did not find an association between muscle radiodensity and muscle protein content in gastrointestinal cancer patients, also potentially explained by a relatively small muscle biopsy compared with the area analysed for muscle radiodensity. Changes in muscle protein and extracellular water content might also affect muscle radiodensity.

Fat is distributed heterogeneously in and around the muscle. This heterogeneous distribution contributes to sampling bias as can be seen at macroscopic level using CT images. Variation in radiodensity and uneven distribution of lipid deposits in the muscle suggest that when investigating muscle at tissue level and fatty infiltration is a measure of interest, precise quantification of amount of lipid in the biopsy is helpful.

Nagao et al. first observed an association between muscle radiodensity and accumulation of fat in infants while investigating techniques for diagnosis of neuromuscular disorders. CT imaging and histochemical analysis has been previously used to exhibit changes in lipid content of leg and thigh muscles in people with obesity and Duchenne muscular dystrophy compared with controls. In the present study, it has been demonstrated that RA radiodensity is indicative of its TG content measured biochemically. This is in line with Goodpaster’s observation of a negative association between mid-thigh muscle radiodensity and TG content of vastus lateralis biopsy in healthy volunteers and diabetic patients. However, that study reported stronger association \( r = -0.580 \) as compared with our observation \( r = -0.396 \). In the prior study, all subjects had muscle radiodensity greater than 25 HU with TG content in the range of 4 and 26 μg/mg. The healthy and diabetic individuals studied were between 25 and 49 years of age. In our study, more than half of the patients had RA radiodensity less than <25 HU with a wider TG content between 0.7 and 88 μg/mg. This could reflect older age of cancer patients (average age of 63 years). We also observed that total lumbar muscle radiodensity at L3, the most commonly analysed CT image cross section for radiodensity that associate to outcomes, is also indicative of total TG content of the muscle. The latter findings should be interpreted with some caution because total muscle radiodensity values at L3 are mixtures of radiodensity values of different muscle groups (i.e. quadratus lumborum, psoas, erector spinae, external obliques, transverse abdominis, internal obliques, and RA) and TG content was analysed for RA only as this is the most common biopsied muscle in cancer patients.

In the current study, the location of lipids in and around the muscle fibres was characterized. Heterogeneous distribution of EMCL and IMCL was observed in the muscle sections. Wide variation in the distribution of lipids within and between muscle fibres suggests that pathways associated with both IMCL and EMCL need to be resolved to delve into the mechanism of fatty infiltration. IMCL is a dynamic pool of lipids in muscle fibre and an important substrate for exercise in endurance athletes. Excess IMCL deposition has been associated with insulin resistance, obesity, inflammation, and muscle dysfunction. Insulin resistance has been associated with predominant deposition of IMCL near cell membrane, large lipid droplet size, and lipid droplet number. EMCL is an accumulation of adipocytes around the muscle fibres and can originate from stem cell populations residing in skeletal muscle. The most well-defined stem cell population in

Figure 5  Mean percentage area of neutral lipids in muscle section analysed using Oil Red O staining in 22 patients. Total area stained for neutral lipids in muscle section was on average 13% (4 to 30%). Out of the total lipid area, the mean proportion of intramyocellular lipid and extramyocellular lipid areas were 46 and 54%, respectively. There were no significant differences in percentage neutral lipid area between male and female patients.
skeletal muscle are satellite cells. However, whether satellite cells adopt adipogenic fate is under debate.

Fibrogenic/adipogenic progenitors, multipotent mesenchymal progenitors, and PW1+ interstitial cells are potential stem cells populations that can contribute to adipocyte development in skeletal muscle.

Computed tomography imaging is an important non-invasive and opportunistic tool in studying lipid infiltration in the muscle in cancer patients. The present study supports the claim made by several studies that low muscle radiodensity is indicative of increased lipid content. However, wide variation in muscle radiodensity demonstrates a cautionary note for future studies using this measure. The reproducibility of muscle radiodensity measure needs to be determined before using it for any analysis. When investigating muscle characteristics at tissue level, biochemical TG extraction and histological ORO staining are more comprehensive and are representative of amount and location of lipid depots. More work is required to understand mechanisms that contribute to muscle lipid accumulation and its effects on muscle physiology.

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Conflict of interest

None declared.

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Online supplementary material

Additional supporting information may be found online in the Supporting Information section at the end of the article.

Table S1: Antibody information used for immunofluorescence experiments: Oil red O

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