Novel Use of Proton Magnetic Resonance Spectroscopy (1HMRS) to Non-Invasively Assess Placental Metabolism

Citation for published version:
Denison, FC, Semple, SI, Stock, SJ, Walker, J, Marshall, I & Norman, JE 2012, 'Novel Use of Proton Magnetic Resonance Spectroscopy (1HMRS) to Non-Invasively Assess Placental Metabolism', *PLoS ONE*, vol. 7, no. 8, e42926. https://doi.org/10.1371/journal.pone.0042926

Digital Object Identifier (DOI):
10.1371/journal.pone.0042926

Link:
Link to publication record in Edinburgh Research Explorer

Document Version:
Publisher's PDF, also known as Version of record

Published In:
*PLoS ONE*

Publisher Rights Statement:
Copyright: © Denison et al. This is an open-access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

General rights
Copyright for the publications made accessible via the Edinburgh Research Explorer is retained by the author(s) and / or other copyright owners and it is a condition of accessing these publications that users recognise and abide by the legal requirements associated with these rights.

Take down policy
The University of Edinburgh has made every reasonable effort to ensure that Edinburgh Research Explorer content complies with UK legislation. If you believe that the public display of this file breaches copyright please contact openaccess@ed.ac.uk providing details, and we will remove access to the work immediately and investigate your claim.
Novel Use of Proton Magnetic Resonance Spectroscopy (1H MRS) to Non-Invasively Assess Placental Metabolism

Fiona C. Denison1*, Scott I. Semple2, Sarah J. Stock1, Jane Walker3, Ian Marshall4, Jane E. Norman1

1 MRC Centre for Reproductive Health, University of Edinburgh, Queen’s Medical Research Institute, Edinburgh, Lothian, United Kingdom, 2 Clinical Research Imaging Centre, University of Edinburgh, Queen’s Medical Research Institute, Edinburgh, Lothian, United Kingdom, 3 Simpson Centre for Reproductive Health, Edinburgh Royal Infirmary, Edinburgh, Lothian, United Kingdom, 4 School of Clinical Sciences, University of Edinburgh, Edinburgh, Lothian, United Kingdom

Abstract

Background: Placental insufficiency is a major cause of antepartum stillbirth and fetal growth restriction (FGR). In affected pregnancies, delivery is expedited when the risks of ongoing pregnancy outweigh those of prematurity. Current tests are unable to assess placental function and determine optimal timing for delivery. An accurate, non-invasive test that clearly defines the failing placenta would address a major unmet clinical need. Proton magnetic resonance spectroscopy (1H MRS) can be used to assess the metabolic profile of tissue in-vivo. In FGR pregnancies, a reduction in N-acetylaspartate (NAA)/choline ratio and detection of lactate methyl are emerging as biomarkers of impaired neuronal metabolism and fetal hypoxia, respectively. However, fetal brain hypoxia is a late and sometimes fatal event in placental compromise, limiting clinical utility of brain 1H MRS to prevent stillbirth. We hypothesised that abnormal placental 1H MRS may be an earlier biomarker of intrauterine hypoxia, affording the opportunity to optimise timing of delivery in at-risk fetuses.

Methods and Findings: We recruited three women with severe placental insufficiency/FGR and three matched controls. Using a 3T MR system and a combination of phased-array coils, a 20×20×40 mm3 1H MRS voxel was selected along the ‘long-axis’ of the placenta with saturation bands placed around the voxel to prevent contaminant signals. A significant choline peak (choline/lipid ratio 1.35–1.79) was detected in all healthy placentae. In contrast, in pregnancies complicated by FGR, the choline/lipid ratio was ≤0.02 in all placentae, despite preservation of the lipid peak (p<0.001).

Conclusions: This novel proof-of-concept study suggests that in severe placental insufficiency/FGR, the observed 60-fold reduction in the choline/lipid ratio by 1H MRS may represent an early biomarker of critical placental insufficiency. Further studies will determine performance of this test and the potential role of 1H-MRS in the in-vivo assessment of placental function to inform timing of delivery.

Introduction

Placental insufficiency is one of the commonest causes of fetal growth restriction (FGR) and antepartum stillbirth. When placental insufficiency is diagnosed antenatally, the only effective treatment is delivery which, if preterm is itself associated with increased morbidity and mortality and considerable financial costs. [1] If placental insufficiency remains undiagnosed and results in stillbirth [2], this can have profound and long lasting consequences for parents and their extended family. [3] One of the main challenges in current obstetric practice is therefore our inability to accurately and non invasively diagnose placental insufficiency, quantify its severity and predict its clinical sequelae. Better diagnosis would improve the timing of clinical interventions and potentially improve perinatal outcome.

In current clinical practice, diagnosis of placental insufficiency and fetal compromise is largely based on Doppler assessment of umbilical artery blood flow, fetal arterial and venous Dopplers (e.g. ductus venosus and middle cerebral artery Doppler waveforms) or ultrasound biometry. [4] Although abnormal Dopplers correlate with cord pH, fetal hypoxia and lactate generation [5], and are associated with the presence of gross placental lesions detectable by ultrasound [6,7], neither Doppler nor conventional ultrasound is able to directly measure placental function. Sibley et al [8] recently proposed that the constellation of physiological and morphological changes may constitute a placental phenotype in some pregnancies complicated with FGR with an abnormal phenotype being associated with poor perinatal outcome. Development of non-invasive tools capable of assessing placental metabolism and cell turnover directly may allow placental phenotyping to occur, thus enabling clinical interventions to be targeted to those pregnancies at highest risk of adverse outcome and timely delivery to be effected.

Magnetic resonance imaging (MRI) is a non-invasive imaging technique which is safe in pregnancy. The technique has the ability to acquire a combination of anatomical information with high spatial resolution, and directly assess a variety of physiological function. MRI is non-invasive and does not involve the use of...
Proton spectroscopy (1H MRS) of Placenta In Vivo

We studied 3 women with a singleton pregnancy complicated by severe FGR and suspected fetal compromise and 3 gestation matched controls. Gestation was calculated from the last menstrual period and confirmed by routine ultrasonography at 11–13 weeks gestation. All participants had a structurally normal fetal anomaly scan at 20 weeks gestation. Severe FGR was defined as an abdominal circumference by ultrasound <5th centile. [15] Suspected fetal compromise was defined as absent or reversed end-diastolic flow on umbilical artery Doppler. Exclusion criteria for study participation included significant co-existing maternal systemic disease including gestational diabetes, microvascular disease, multiple pregnancy, or contraindication to MRI.

Magnetic Resonance Studies

All magnetic resonance (MR) studies were performed using a wide-bore dedicated clinical research 3 tesla MR Verio system (Siemens Medical, Germany). Women were scanned in a left-lateral tilt to avoid compression of ven-a-cava with blood pressure constantly monitored using a Veris MR Vital Signs Monitor (Mead, UK). Total MR acquisition times were limited to 40–45 minutes per participant. No fetal sedation was used. A combination of body and spine matrix phased-array coils was used to obtain all images and 1H MRS data. Prior to acquisition of 1H MRS data, a series of 2D HASTE slices was acquired in three orthogonal planes centred on the placenta. Multiple 6 mm slices were acquired with no inter-slice gap in all three planes, in order to localise the extent of the placenta. Each HASTE image took approximately 1 second to acquire, so all images were acquired with the mother free-breathing.

MR Spectroscopy Studies

For 1H MRS acquisition, a 20×20×40 mm PRESS voxel was selected along the ‘long-axis’ of the placenta (TE/TR 144/1500 ms, 96 averages). The voxel was selected approximately 2 cm from the cord insertion in all cases and voxel selection was confirmed to be limited to within the placenta using the range of orthogonal HASTE slices (Figure 1). Six saturation bands were placed around the voxel to further prevent any non-placenta contaminant signals and a second-order semi-automatic shim was applied over the selected voxel to counter any local inhomogeneities in the magnetic field. The voxel dimensions were selected to maximise sampling of the placental unit, thereby increasing signal-to-noise values of the resulting spectra. 1H MRS data was acquired with the mother free-breathing. In our experience, the placental unit does not significantly move outwith our selected voxel dimensions during either maternal breathing, or fetal motion. The resulting raw spectral data was exported to an external workstation and MRS analysis to assess placental metabolism (Lipid/choline ratio) was quantified using the Java-based MRS analysis tool JMRUI (http://www.mrui.uab.es/mrui).

Data Analysis

The 1H MRS quantification process was performed using the nonlinear least-squares quantitation algorithm AMARES (Advanced Method for Accurate, Robust and Efficient Spectral fitting) with peak fitting performed assuming a Lorentzian line shape. Since only two peaks were clearly identified, each peak was identified manually according to its frequency and the line widths and areas under the curves semi-automatically estimated. Birth percentiles were calculated using centile charts for birthweight for gestational age for Scottish singleton births. [16] Data were analysed by GraphPad Prism (Version 5.0).

Methods

Ethics Statement

The study was approved by Lothian Research Ethics Committee (10/S1103/36) and all participants gave written, informed consent.

Study Population

Patients were enrolled at the Simpson Centre for Reproductive Health at the Royal Infirmary, Edinburgh, UK. Magnetic resonance imaging (MRI) studies were performed at the Clinical Research Imaging Centre in the Queen’s Medical Research Institute, University of Edinburgh, Edinburgh, UK.

MRS. in normal pregnancy and those complicated by FGR using 1H attempted to assess the metabolic footprint of the placenta hypoxia [13,14], we are not aware of any studies which have turnover may precede the onset of placental and intrauterine suggest that altered placental metabolism and reduced cell impaired neuronal metabolism. [12] Although species, reduction in NAA/choline ratio is emerging as a biomarker of information as an image, 1H MRS instead provides data on the return to their original state, the resulting radiofrequency signal is determined by the MR system. [11] Whilst MRI produces information as an image, 1H MRS instead provides data on the relative concentrations of specific metabolites contained within selected regions of interest, with the local chemical and magnetic environment in which each proton is situated within that region determining the ‘chemical shift’ in resonant frequency that each proton’s signal exhibits after excitation. This chemical shift data is expressed as a frequency spectrum with contributions of specific metabolites appearing as individual peaks at discrete frequencies. The area under each frequency peak is proportional to the number of protons, and hence the concentration, of the metabolite. 1H MRS therefore has the potential to be a powerful, non-invasive method of assessing the metabolic profile of tissue in vivo.

In healthy pregnancies, a choline peak detected by 1H MRS is associated with a normal high degree of cell-turnover in the developing fetal brain whilst an increasing N-acetylaspartate (NAA) peak with gestational age reflects the increase in the number of neurons during brain development. In FGR pregnancies, reduction in NAA/choline ratio is emerging as a biomarker of impaired neuronal metabolism. [12] Although in vitro studies suggest that altered placental metabolism and reduced cell turnover may precede the onset of placental and intrauterine hypoxia [13,14], we are not aware of any studies which have attempted to assess the metabolic footprint of the placenta in normal pregnancy and those complicated by FGR using 1H MRS.

The aim of our study was therefore to establish the feasibility of undertaking 1H MRS of the placenta in vivo, and to undertake the first proof-of-concept study to assess whether the metabolic footprint of the placenta differs in placenta from pregnancies complicated by FGR compared to healthy controls.
Results

Demographics of Study Population

Maternal age ranged between 20 and 37 (mean, 28±6.8 years) and maternal body mass index (BMI) between 18.4 and 32.8 (mean, 25.7±4.8 kg/m²). The demographics of the study population at the time of MRS scan and delivery are demonstrated in Tables 1 and 2. Neonatal outcome and time between ¹H MRS and delivery are demonstrated in Table 3.

MRI Results

In utero ¹H MRS of the placenta was obtained in all participants. A choline and lipid peak were easily detectable, centred at 3.2 ppm and 1.2 ppm, respectively from placentae in all healthy controls (Figure 2). In the healthy controls a significant choline signal was obtained, resulting in a choline/lipid ratio of 1.35–1.79. In contrast, despite preservation of the lipid peak, there was severe attenuation or absence of detectable choline peak in placentae from pregnancies complicated by severe FGR and suspected fetal compromise (Figure 3). The choline/lipid ratio was reduced to ≤0.02, a reduction of more than 60-fold in pregnancies

Table 1. Maternal demographics, gestational age and antenatal Dopplers at the time of ¹H MRS.

| Subject      | Age | Parity | BMI | Abdominal circumference ultrasound centile | Umbilical artery | Liquor volume | Gestational age at ¹H MRS (wks+days) |
|--------------|-----|--------|-----|------------------------------------------|------------------|---------------|-------------------------------------|
| Healthy 1    | 33  | 0+0    | 18.4| 25⁰–50⁰                                  | Normal           | Normal        | 24⅔                          |
| Healthy 2    | 31  | 1+0    | 23.1| 50⁰–95⁰                                  | Normal           | Normal        | 30⅓                          |
| Healthy 3    | 37  | 2+1    | 25.3| 50⁰–95⁰                                  | Normal           | Normal        | 28⅔                          |
| Compromised 1| 30  | 0+0    | 23.1| <5⁰                                     | AEDF             | Reduced       | 28⅔                          |
| Compromised 2| 20  | 0+1    | 26.4| <5⁰                                     | AEDF             | Reduced       | 25⅓                          |
| Compromised 3| 23  | 0+1    | 32.8| <5⁰                                     | AEDF             | Reduced       | 27⅔                          |

AEDF (absent end diastolic flow).

doi:10.1371/journal.pone.0042926.t001
complicated by severe FGR compared to the gestation matched healthy controls (Table 3) (p<0.001).

Discussion

To our knowledge, this is the first report of placental $^1$H MRS in vivo in normal and FGR pregnancies. We demonstrate that in healthy pregnancies, choline and lipid spectral peaks were clearly detected in all placenta using $^1$H MRS. In contrast, in pregnancies complicated by FGR, despite preservation of the lipid peak, the choline peak was severely attenuated or absent from all placentae. We speculate that a reduction in the choline/lipid ratio by $^1$H MRS may provide a novel biomarker of critical placental failure, indicative of reduction in cell turnover, which predates fetal hypoxia and antepartum stillbirth in pregnancies with severe FGR.

To date, knowledge about placental function in FGR pregnancies has been largely extrapolated from in vitro and ex vivo studies. Placental weight, total volume, villous volumes and surface area are significantly reduced in FGR pregnancies. [17] At a histological level, there is evidence of increased apoptosis, a thickened basal lamina and reduction in cytotrophoblastic nuclei and cell-turnover. [14,18] The marked impairment of nutrient transport [13,19] and placental perfusion which occurs results in global placental dysfunction and altered metabolism [20,21]. Cetin et al suggested that such alterations in placental metabolism and function may precede the onset of placental and intrauterine hypoxia in affected pregnancies. [13] If it were possible to detect altered placental metabolism prior to the onset of critical placental failure, this might afford an opportunity for more timely clinical intervention (including delivery) thus preventing adverse perinatal outcome.

A variety of non-invasive methods have attempted to assess placental function in vivo to predict the functional capacity of the pregnancy and/or pregnancy outcome. The ultrasound based ‘Grannum grading’ of placenta, which was originally developed as a biomarker for fetal lung maturity, has been assessed as a predictive tool for fetal growth restriction [22] and placental function [23]. However, although there is a relationship between Grannum III grade and FGR, the positive predictive and sensitivity value of this “test” is low (62% and 66%, respectively) [22] and Grannum grading at 31–34 weeks of gestation is unable to reliably predict the functional capacity of the term placenta as expressed by the surrogate measure, morphometric diffusive conductance. [23] More recently, near infrared spectroscopy has been explored as potential method of assessing tissue oxygenation and placental function. [24–26] To date, results have been conflicting in FGR pregnancies with tissue oxygenation indexes exhibiting both increase and decrease in the presence of FGR depending on its cause. [24–25] Furthermore, due to technical limitations, the latter technique is only able to assess placental oxygenation within a narrow range and in women with an anterior placentae and a thin layer of subcutaneous fat. [24] Until further method development occurs, these techniques are therefore unlikely to have a clinical utility in quantifying placental oxygenation and function in vivo.

Several groups have used MRI as a tool for assessing fetal and placental structure and function in vivo. At the macroscopic level, placental volume measured by MRI during the second trimester

### Table 2. Characteristics of population at delivery.

| Subject          | Gestational age at delivery, wks +/- days | Mode delivery | Sex  | Fetal weight (g) | Percentile at birth |
|------------------|------------------------------------------|---------------|------|------------------|---------------------|
| Healthy 1        | 40 +/- 0                                  | SVD           | Male | 3060             | 25<sup>th</sup>     |
| Healthy 2        | 40 +/- 3                                  | SVD           | Male | 3760             | 50<sup>th</sup>     |
| Healthy 3        | 39 +/- 5                                  | SVD           | Male | 3630             | 50<sup>th</sup>     |
| Compromised 1    | 30 +/- 4                                  | SVD           | Male | 750              | <0.4<sup>th</sup>   |
| Compromised 2    | 25 +/- 4                                  | EmCS          | Male | 670              | 9<sup>th</sup>      |
| Compromised 3    | 28 +/- 6                                  | EmCS          | Male | 530              | <0.4<sup>th</sup>   |

SVD (spontaneous vertex delivery), EmCS (emergency caesarean section).

doi:10.1371/journal.pone.0042926.t002

### Table 3. Neonatal outcome and choline/lipid integral $^1$H MRS ratio.

| Subject          | Outcome                        | Time between $^1$H MRS and delivery (days) | Choline/lipid integral ratio |
|------------------|--------------------------------|--------------------------------------------|-----------------------------|
| Healthy 1        | Alive and well                 | 108                                        | 1.35                        |
| Healthy 2        | Alive and well                 | 70                                         | 1.79                        |
| Healthy 3        | Alive and well                 | 82                                         | 1.36                        |
| Compromised 1    | Stillbirth<sup>1</sup>         | 13                                         | <0.02                       |
| Compromised 2    | Neonatal death at 42 days      | 4                                          | <0.02                       |
| Compromised 3    | Discharged from NNU with BPD and ROP on supplemental oxygen at 42<sup>++</sup> weeks corrected gestation | 12                                         | 0.02                        |

<sup>1</sup>Compromised 1 pregnancy was expectantly managed until antenatal stillbirth occurred.

NNU (neonatal unit), BPD (bronchopulmonary dysplasia), ROP (retinopathy of prematurity).

doi:10.1371/journal.pone.0042926.t003
correlates with uterine artery perfusion and is reduced in pregnancies that subsequently delivered FGR infants. [27] Furthermore, the severity of FGR and incidence of fetal or neonatal mortality has been shown to correlate with the MR volume of placenta affected by pathology. [28] More recently Wright et al demonstrated that placental relaxation times (T1 and T2) were negatively correlated with gestation. [29] However, when the relaxation times were compared to postnatal examination, T2 only correlated with placental fibrin deposition if the scan and delivery were within one week of each other.

Studies using MRI to assess placental function are more limited. Bonel et al report that reduced apparent diffusion coefficient (ADC) as measured by diffusion-weighted MRI is exhibited in placental dysfunction associated with FGR. The authors hypothesised that placenta dysmaturity and focal disruption of the placental barrier which occur in FGR was responsible for the altered diffusion [30]. Using the technique of intravoxel incoherent motion and perfusion fraction mapping, Moore et al identified differences in function within the normal placenta in vivo, and between the placentae of normal and IUGR pregnancies. [31] Finally, using gadoterate melamine for contrast enhancement, Brunelli et al demonstrated that intervillous circulation was severely compromised in pregnancies with severe FGR. [32] However, this study was undertaken only a few hours prior to

![Figure 2. 2x2x4 cm voxel MRS acquired at 144 ms from placenta from healthy participant 1. In this case, choline and lipid spectral peak demonstrated at frequencies of 3.21 ppm, and 1.3 ppm and 0.9 ppm per million (ppm) respectively. doi:10.1371/journal.pone.0042926.g002](Image)
delivery by caesarean section due to concerns about fetal toxicity of gadolinium-based contrast agents, which are not licenced for use in pregnancy. None of these MRI techniques assess placental metabolism and function directly.

$^1$H MRS by comparison to MRI is able to dynamically assess levels of specific metabolites in the region of interest selected. To date, the use of $^1$H MRS during pregnancy has been restricted to assessment of the fetal brain in health and disease. In pregnancies complicated by FGR, a reduction in NAA/choline in the fetal brain is thought to be indicative of impaired neuronal metabolism and reduced cell-turn over [12], and the presence of lactate methyl [33] to be indicative of established fetal hypoxia. However, both of these 'biomarkers' are likely to develop relatively late in the evolution of fetal compromise and hypoxia, limiting opportunities for therapeutic intervention.

To our knowledge, $^1$H MRS has not been previously undertaken in the placenta in vivo. We demonstrate that in FGR pregnancies with suspected compromise, despite preservation of the lipid peak, there is a severe reduction or absence of a placental choline peak. This is in contrast to healthy pregnancy where choline and lipid peaks are readily detectable. The presence of choline by $^1$H MRS in organs including the fetal brain is thought to indicate cell-turnover and growth. [34] In contrast, a reduction in the choline peak (compared to baseline) occurs when cell

Figure 3. 2×2×4 cm voxel MRS acquired at 144 ms from placenta from compromised participant 2. Lipid spectral peak demonstrated at frequency of 1.42 ppm. Choline peak below level of reliable detection. doi:10.1371/journal.pone.0042926.g003
turnover is significantly reduced and in the presence of apoptosis. [35] Using ex vivo and in vitro models, Heazzel et al [36] and others [19] [14] have demonstrated a reduction in cell-turnover and increase in apoptosis in placentae from pregnancies with FGR. We therefore propose that the significant reduction in choline/lipid ratio which we demonstrate in FGR, placentae may be a novel biomarker of reduced cell turnover before apoptosis resulting in impaired placental function and critical organ failure.

Acquiring the 1H MRS data at 3T had the added benefit of the increased signal to noise available at this higher clinical field strength. This meant that less averages were required to obtain an acceptable signal-to-noise ratio for our 1H MRS data. Modern clinical 3T systems also allow rapid and accurate magnetic shimming to correct for static field inhomogeneities. This meant that an entire MRI and 1H MRS placental examination could be obtained with a 40-minutes total acquisition time.

Although our study is limited by small numbers, we were able to detect a reproducible spectral output from placentae from all the women that were scanned, regardless of placental site and size, fetal motion and maternal habits. However, for this proof-of-concept study we specifically recruited women with severe FGR who had evidence of fetal compromise and growth measurements <5th centile. All babies with severe FGR had poor outcomes. To assess the clinical utility of 1H MRS as a diagnostic tool for placental failure, future studies should recruit women with less severe FGR to assess whether there is a lipid/choline ratio below which risk of adverse perinatal outcome increases.

In conclusion, our proof-of-concept study demonstrates that the MRS spectra of placentae in pregnancies complicated by severe FGR are significantly different from those from healthy pregnancies. Future studies should explore whether the absence of a choline peak represents a biomarker of critical placental failure and the consequence of this for perinatal outcome.

**Acknowledgments**

We would also like to thank Isobel Crawford, Mary Simpson and Jennifer Rowan for recruiting women to take part in this study. Finally, we would like to thank the radiographers at the Clinical Research Imaging Centre for facilitating and performing the MRI scans.

**Author Contributions**

Conceived and designed the experiments: FCD SIS JEN IM JW. Performed the experiments: FCD SIS IM JW. Analyzed the data: FCD SIS JEN IM. Contributed reagents/materials/analysis tools: FCD SIS JEN IM. Performed the 1H MRS: FCD JEN. Contributed to data collection and to the virology specimens: SIS JEN IM. IM. Wrote the paper: FCD SIS JEN IM JW SJS.

**References**

1. Mangham LJ, Petrou S, Doyle LW, Draper ES, Markow N (2009) The cost of preterm birth throughout childhood in England and Wales. Pediatrics 123: c312–327.
2. Sankaran S, Kyle PM (2009) Artiopathy and pathogenesis of IUGR. Best Pract Res Clin Obstet Gynaecol 23: 765–777.
3. Schott J, Henley A After a late miscarriage, stillbirth or neonatal death. J Fam Health Care 20: 116–118.
4. Chalubinski KM, Repa A, Stammli-Hafner M, Ott J (2011) The impact of doppler sonography on intrauterine management and neonatal outcome in preterm fetuses with intrauterine growth retardation. Ultrasound Obstet Gynecol.
5. Semple SI, Wallis F, Haggarty P, Abramovich D, Ross JA, et al. (2001) The measurement of fetal liver T(2)% in utero before and after maternal oxygen breathing: progress towards a non-invasive measurement of fetal oxygenation and placental function. Magn Reson Imaging 19: 921–928.
6. Sebire NJ, Sepulveda W (2008) Correlation of placental pathology with prenatal ultrasound findings. J Clin Pathol 61: 1276–1294.
7. Madzzi R, Somunkiran A, Calay Z, Iivan S, Akas MF (2003) Histomorphology of the placenta and the placental bed of growth restricted foetuses and correlation with the Doppler velocimities of the umbilical and umbilical arteries. Placenta 24: 510–516.
8. Sibley CP, Turner MA, Cetin I, Ayuk P, Boyd CA, et al. (2005) Placental phenotypes of intrauterine growth retardation. Pediatr Res 58: 827–832.
9. Teo TH, Law YM, Tai KH, Tan BS, Cheah FK (2009) Use of magnetic resonance imaging in evaluation of placental invasion. Clin Radiol 64: 511–516.
10. Bonel HM, Stolz B, Dietrichsen I, Frei K, Saar B, et al. (2011) Diffusion-weighted MR imaging of the placenta in fetuses with placental insufficiency. Radiology 257: 808–819.
11. Story L, Damodaram MS, Allopp JM, McGuinness A, Wylezinska M, et al. (2011) Proton magnetic resonance spectroscopy in the fetus. Eur J Obstet Gynecol Reprod Biol 158: 3–8.
12. Story L, Damodaram MS, Allopp JM, McGuinness A, Patel A, et al. (2011) Brain metabolism in fetal intrauterine growth restriction: a proton magnetic resonance spectroscopy study. Am J Obstet Gynecol 205: 483 e481–488.
13. Cetin I, Alvino G (2009) Intrauterine growth restriction: implications for placental metabolism and transport. A review. Placenta 30 Suppl A: S77–92.
14. Macara L, Kingdom JC, Kauffmann P, Kohane G, Hui J, et al. (1996) Structural analysis of placental terminal villi from growth-restricted pregnancies with abnormal umbilical artery Doppler waveforms. Placenta 17: 37–48.
15. Loughnna P, Chitty L, Evans T, Chudleigh T (2009) Fetal size and dating: charts recommended for clinical obstetric practice. Ultrasound 17: 161–167.
16. Bonel HM, Schlemmer J, Greer I, Jarvis S, et al. (2008) Fetal centile chart for birthweight for gestational age for Scottish singleton births. BMC Pregnancy Childbirth 8: 3.
17. Eghbali M, Amini T, Morris N, Green CJ, Sibson PD (2006) Morphometric placental villous and vascular abnormalities in early- and late-onset preeclampsia with and without fetal growth restriction. BJOG 113: 580–589.
18. Smith SG, Baker PN, Symonds EM (1997) Increased placental apoptosis in intrauterine growth restriction. Am J Obstet Gynecol 179: 1385–1401.
19. Horgan RP, Broadhurst DJ, Dunn WB, Brown M, Heazzel AE, et al. (2010) Changes in the metabolic footprint of placental explant-conditioned medium cultured in different oxygen tensions from placentae of small for gestational age and normal pregnancies. Placenta 31: 993–901.
20. Dunn WB, Brown M, Horton SA, Crocker IP, Broadhurst D, et al. (2009) Changes in the metabolic footprint of placental explant-conditioned culture medium identifies metabolic disturbances related to hypoxia and pre-eclampsia. Placenta 30: 974–980.
21. Heazzel AE, Brown M, Dunn WB, Horton SA, Crocker IP, et al. (2009) Analysis of the metabolic footprint and tissue metabolome of placental villous explants cultured at different oxygen tensions reveals novel redox biomarkers. Placenta 29: 691–698.
22. Yin TS, Loughnna P, Ong SS, Padfield J, Millroy TM (2009) No correlation between ultrasound placental grading at 31–34 weeks of gestation and a surrogat estimate of organ function at term obtained by stereological analysis. Placenta 30: 726–730.
23. Kazi GM, Gross TL, Sokol RJ, Kazi NJ (1983) Detection of intrauterine growth retardation: a new use for sonographic placental grading. Am J Obstet Gynecol 145: 733–737.
24. Hasegawa J, Nakamura M, Matsuo R, Mimura T, Ichizuka K, et al. (2010) Evaluation of placental function using near infrared spectroscopy during fetal growth restriction. J Perinat Med 38: 29–32.
25. Kakogawa J, Sumimoto K, Kawamura T, Minosa S, Kanayama N (2010) Noninvasive monitoring of placental oxygenation by near-infrared spectroscopy. Am J Perinatol 27: 463–468.
26. Kakogawa J, Sumimoto K, Kawamura T, Minosa S, Kanayama N (2010) Transabdominal measurement of placental oxygenation by near-infrared spectroscopy. Am J Perinatol 27: 25–29.
27. Derwig IE, Akelekar R, Zelaya FO, Gowland PA, Barker GJ, et al. (2011) Association of placental volume measured by MRI and birth weight percentile. J Magn Reson Imaging 34: 1125–1130.
28. Damodaram M, Story L, Einzeh E, Patel A, McGuinness A, et al. (2010) Placental MRI in intrauterine fetal growth restriction. Placenta 31: 491–498.
29. Wright C, Morris DM, Baker PN, Crocker IP, Gowland PA, et al. (2011) Magnetic resonance imaging relaxation time measurements of the placenta at 1.5 T. Placenta 32: 1010–1015.
30. Bonel HM, Stolz B, Dietrichsen I, Frei K, Saar B, et al. (2010) Diffusion-weighted MR imaging of the placenta in fetuses with placental insufficiency. Radiology 257: 810–819.
31. Moore RJ, Strachan BK, Tyler DJ, Duncan KR, Baker PN, et al. (2000) In utero perfusion fraction maps in normal and growth restricted pregnancy measured using IVIM echo-planar MRI. Placenta 21: 726–732.
32. Brunelli R, Masselli G, Parasassi T, De Spirito M, Papa M, et al. (2010) Intervillous circulation in intra-uterine growth restriction. Correlation to fetal well being. Placenta 31: 1051–1056.
33. Cetin I, Barberis B, Brusati V, Brighina E, Mandia L, et al. (2011) Lactate detection in the brain of growth-restricted fetuses with magnetic resonance spectroscopy. Am J Obstet Gynecol 205: 350 e351–357.
34. Brighina E, Bresolin N, Pardi G, Rango M (2009) Human fetal brain chemistry as detected by proton magnetic resonance spectroscopy. Pediatr Neurol 40: 327–342.

35. Lindskog M, Spenger C, Klason T, Jarvet J, Gradlund A, et al. (2005) Proton magnetic resonance spectroscopy in neuroblastoma: current status, prospects and limitations. Cancer Lett 228: 247–255.

36. Heazell AE, Sharp AN, Baker PN, Crocker IP (2011) Intra-uterine growth restriction is associated with increased apoptosis and altered expression of proteins in the p53 pathway in villous trophoblast. Apoptosis 16: 135–144.