Patient-Derived Nasopharyngeal Cancer Organoids for Disease Modeling and Radiation Dose Optimization

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Effective radiation treatment (RT) for recurrent nasopharyngeal cancers (NPC), featuring an intrinsic hypoxic sub-volume, remains a clinical challenge. Lack of disease-specific in-vitro models of NPC, together with difficulties in establishing patient derived xenograft (PDX) models, have further hindered development of personalized therapeutic options. Herein, we established two NPC organoid lines from recurrent NPC PDX models and further characterized and compared these models with original patient tumors using RNA sequencing analysis. Organoids were cultured in hypoxic conditions to examine the effects of hypoxia and radioresistance. These models were then utilized to determine the radiobiological parameters, such as $\alpha/\beta$ ratio and oxygen enhancement ratio (OER), characteristic to radiosensitive normoxic and radioresistant hypoxic NPC, using simple dose-survival data analytic tools. The results were further validated in-vitro and in-vivo, to determine the optimal boost dose and fractionation regimen required to achieve effective NPC tumor regression. Despite the differences in tumor microenvironment due to the lack of human stroma, RNA sequencing analysis revealed good correlation of NPC PDX and organoid models with patient tumors. Additionally, the established models also mimicked inter-tumoral heterogeneity. Hypoxic NPC organoids were highly radioresistant and had high $\alpha/\beta$ ratio compared to its normoxic counterparts. In-vitro and in-vivo fractionation studies showed that hypoxic NPC was less sensitive to RT fractionation scheme and required a large bolus dose or 1.4 times of the fractionated dose that was effective against normoxic cells in order to compensate for oxygen deficiency. This study is the first direct
experimental evidence to predict optimal RT boost dose required to cause sufficient damage to recurrent hypoxic NPC tumor cells, which can be further used to develop dose-painting algorithms in clinical practice.

Keywords: recurrent NPC, organoids model, radioresistance, oxygen enhancement ratio, hypoxia, linear quadratic model, patient-derived xenografts, radiotherapy

INTRODUCTION

Nasopharyngeal carcinoma (NPC) is endemic in the east and southeast Asia, where 95% of the cases are invariably associated with Epstein-Barr virus (EBV) infection (1). Radiotherapy (RT) has been the mainstay treatment for early-stage NPC. However, >50% of the patients present with locally advanced and distant metastasis during initial diagnosis, reducing the 5-year survival rates to 50–70% (2). Local recurrences are observed in ~10% of the patients following initial RT, representing a substantial challenge to oncologists (3, 4). Re-treatment with RT (dose ≥60 Gy) is employed in 70–80% of inoperable advanced recurrent cases (5), often resulting in late complications (6–8), further reducing the 5-year survival to ≤50% (9–11). Hence, there is an urgent need for optimized treatment combination and personalized RT planning to achieve local tumor control without significant late morbidities in advanced recurrent NPC.

With significant advancements in diagnostic technology, suboptimal doses and marginal misses may not be the principal cause for local failure. In fact, most locoregional recurrences occurred in the high dose region of the gross tumor volume (GTV) (12), suggesting a strong biological relationship between clonal selection and proliferation of radioresistant cells at the primary site (13). This could be linked to the intrinsic radioresistant hypoxic environment of recurrent NPC, which in turn compromises radiation induced cellular damage and apoptosis; resulting in angiogenesis, tumor progression, and radioresistance (14).

Prevention of recurrence due to hypoxic cell survival may require a higher radiation dose to hypoxic sub-volumes to compensate for oxygen insufficiency. Nevertheless, it remains unclear how much boost dose is required to eliminate hypoxic NPC cells and whether they are sensitive to dose fractionation. Although, the α/β ratio of NPC tissue is generally assumed to be 10 Gy (15), there is no experimental evidence determining the radiobiological parameters specific to NPC tissues or the optimal dose escalation required to eliminate radioresistant cells in the hypoxic sub-volume.

Here in, we established in-vitro hypoxic organoids models, mimicking the hypoxic radioresistant sub-volumes of recurrent NPC. We then employed simple and straightforward radiation dose-survival data analytic techniques that yields quantitative readouts defining the inherent radiobiological parameters, such as α/β ratio and oxygen enhancement ratio (OER) of radiosensitive normoxic and radioresistant hypoxic NPC. We then validated the effectiveness of the experimentally calculated RT boost dose in controlling the growth of in-vitro and in-vivo patient derived NPC tumor models to determine an optimal boost dose and fractionation regimen to obliterate the radioresistant hypoxic cells.

MATERIALS AND METHODS

NPC Patient Participants and Samples

Eighteen NPC tissue samples were obtained from patients who underwent biopsy or surgical resection at the National University Hospital Singapore between March 2015 and April 2019. Specimen collection and experimental use were approved by the Institutional Review Board of National Healthcare Group (DSRB Reference: 2015/00098-SRF0004). One part of the tissue collected from patients were immediately transferred to RPMI-1460 media with HEPES and L-Glutamine and 5X antibiotic/antimycotic and 5 μg/ml Metronidazole at 4°C. Other part was fixed in 10% neutral buffered formalin (10% NBF) for routine Hematoxylin and Eosin (H&E) staining and remaining tissues were snap frozen in liquid nitrogen for DNA and RNA extraction.

NPC PDX Implantation

NPC patient sample was cut into 4–5 mm pieces and immersed in 1:1 Geltrex : HBSS (Gibco). For subcutaneous implantation, 2–3 mm nick was made on the skin of an anaesthetized NSG mice to insert the explanted tissue. For renal capsular implantation, an incision was made in the mouse kidney to insert the tumor tissue in the subcapsular space. All animal care and experimental procedures were approved by the Institutional Animal Care and Use Committee, A*Star Research Entities, Singapore.

Establishment of Organoid Cultures

A modified cancer tissue-originated spheroid (CTOS) method was adopted for establishment of NPC organoids from xenograft tumors (Figure 1A) (16). Briefly, PDX tissues were manually minced into 1–2 mm³ pieces and subjected to enzymatic digestion using 0.28 U/ml Liberase DH (Roche) in RPMI-1460 containing 5% Penicillin-Streptomycin, 20 mM HEPES, 5 U/ml DNase1, and 30 μM Y-27632 (Stemcell Technologies) for 1.5 h at 37°C. The tissue digest was then resuspended in ice-cold HBSS with 5 U/ml DNase1 and 30 μM Y-27632. To remove large undigested pieces, the cell suspension was filtered through 100 μm cell strainer, followed by isolation of the 70–100 μm and 30–70 μm fractions using 70 μm and 30 μm MACS Smart Strainer (Miltenyi Biotech) respectively. Organoids were then counted and then gently mixed with Geltrex (Gibco) at 1.2% (w/v). Fifty microliters of the organoid suspension was seeded in 96-well ultra-low attachment plates (Corning). The gel matrix was then overlaid with 200 μl of complete PneumaCult™-ALI (P-ALI)
media (Stemcell Technologies) supplemented with niche factors (NF): 4 μg/ml Heparin, 125 ng/ml Hydrocortisone, 50 ng/ml EGF, 50 ng/ml bFGF, 20 ng/ml FGF-10, 10 μM SB 202190, 500 nM A83-01, 10 μM Y-27632, and 2 mM Glutamax.

**C666-1 Cell Monolayer and Spheroids Culture**

C666-1 cells (RRID: CVCL_7949) were authenticated using STR (Short tandem repeat) profiling and were free of mycoplasma contamination. The cells were cultured in RPMI-1640 medium supplemented with 10% FBS at 37°C in a humidified incubator under 5% CO2. Confluent cells (70–80%) were sub-passaged by incubation with 0.05% trypsin for 5 min at 37°C and a splitting ratio of 1:3 was used. For monolayer cultures of C666-1 in 96-well high binding flat bottom plates, cells were seeded at a concentration of 5,000 cells/well. For spheroid cultures, cells were seeded in 96-well flat bottomed ultra-low attachment plates at a concentration of 8,000 cells/well.

**RNA Sequencing and Analysis**

Approximately 1 μg RNA per sample (patient biopsy, PDX tumors, organoids, and cell-line) was used to construct the complementary (cDNA) library. Briefly, for all the patient samples, total RNA samples extracted from tissues, except for one patient RNA sample (250T) RNA was extracted from formalin fixed paraffin embedded (FFPE) tissue. Ribosomal
RNA (rRNA) was removed from total RNA using Ribo-zero™ RNA Removal Kit (Epitect, Madison, WI, USA). For the other RNA samples from PDX tissues, organoid, and cells, rRNA depletion was not carried out. Strand-specific RNA-seq libraries were prepared using the NEBNext® Ultra™ Directional RNA Library Prep Kit for Illumina® (NEB, UK), as per manufacturer’s instructions. Sequencing was performed on an Illumina® with NovaSeq 6000 (Illumina, USA) to generate 150 bp paired-end reads. For patient samples, coding and long non-coding RNA was sequenced, whereas only the coding mRNA was sequenced for all other samples.

Raw.fastq sequencing results are separated into human and mouse reads using Xenome with hg19 human genome and GRCh38 p6 mouse genome. Reads mapped exclusively to human are aligned to Gencode hg19 transcriptome using STAR and quantified by RSEM to obtain FPKM (Fragments Per Kilobase per Million mapped reads) and raw counts per gene for downstream analyses. Only the protein coding genes (n = 20,330) were considered.

**Differential Gene Expression and Functional Enrichment**

Gene ontology (GO) analysis was performed with Gene Set Enrichment Analysis (GSEA) when inferring from the whole protein-coding transcriptome, or with g:Profiler when inferring from a subset of labeled genes. We separately performed GO analysis using the GSEA Hallmark gene set, Kyoto Encyclopedia of Genes and Genomes (KEGG) annotations, ontology of biological processes (GO : BP), and cellular components (GO : CC).

For GSEA, the input matrix was the read counts per gene calculated from RSEM, which was then normalized by size factor estimation from DESeq2 on a per-sample basis. Due to the limited number of available samples, false-discovery rate was controlled by permuting the gene sets instead of phenotypes. Ontologies with a family-wise error rate (FWER) <0.05 were deemed significantly different between phenotypes.

Principal component analysis (PCA) was used in discerning the inter-sample differences. Principal components were calculated from the top 1,000 most dispersed protein-coding genes, measured by the log mean-variance ratio (logVMR) of the log-FPKM expression values from RSEM. The ontology of genes contributing to the top principal components (PC) are further considered using g:Profiler. The analysis was separated by the positive and negative contributions to the PC, and ontology were deemed significantly different with adjusted p-value <0.05.

**In-Vitro Single Dose RT**

All irradiation was performed using Gammasell with ¹³⁷Cs source (Nordion, Canada) at a dose rate of 1 Gy/min with ±15% error. To determine the radiobiological parameters of NPC, C666-1 monolayer and spheroids cultures as well as organoids, were irradiated once at doses ranging from 0.2 to 30 Gy on Day 5. Cell viability was measured on days 14 and 21 using the RealTime-Glo™ MT Cell Viability Assay and percentage of viable cells were expressed relative to that in the untreated well.

**Cell Viability Assays**

C666-1 cell, C666-1 spheroid, and NPC organoid viability was determined by RealTime-Glo™ MT Cell Viability Assay (Promega) following manufacturer’s protocol. Briefly, old culture media was replaced with 200 μl of respective culture media containing MT Cell Viability Substrate and NanoLuc® Enzyme at 1X concentration. For monolayer culture, the luminescence measurements could be taken from 1 h following the addition of the reagents but for 3D cultures a minimum of 6 h incubation was required. Luminescence values of the treated group were normalized to respective control non-irradiated organoids grown in normoxic and hypoxic conditions. This ATP independent cell-viability assay was employed to determine the dose-response survival following irradiation of the cells/organoids. A complementary CellTiter-Glo® 3D cell viability assay was used as an end-point assay for 3D cultures following manufacturer’s protocol with some modification. Briefly, 50 μl of 5 U/ml Dispase (Stemcell Technologies) was added to each well to digest the gel and the plate was incubated at 37°C for 45 min. One hundred microliters of Cell-Titre glo 3D reagent was added and incubated for another 1 h at 37°C before measuring the luminescence using a plate reader.

A Live/dead cell imaging assay was also done to qualitatively determine the number of live and dead cells using Live/Dead® viability/cytotoxicity kit (Molecular Probes) following manufacturer’s protocol. Briefly, 2 μM calcine AM and 4 μM Ethidium Homodimer-1 in sterile, tissue culture grade D-PBS were added to the well directly and incubated for 1 h before imaging using a fluorescent microscope with standard FITC and TRITC filters. Samples were washed two more times with HBSS before mounting on eight-well chambered cover glass slide (μ-Slide 8 Well, ibidi®).

**In-Vivo RT**

Fifty NOD Scid Gamma (NSG) mice (5–6 weeks old, 22 ± 2 g) were subcutaneously implanted with NPC PDX tissues at the left flank. When the tumors reached an average size of about 200 mm³, the mice were randomly assigned to six groups (seven mice per group) (i) Control (20% v/v DMSO in saline); (ii) Chemotherapy (CT) alone—5 mg/kg Cisplatin (Cis) and 100 mg/kg 5-Fluorouracil (5-FU) dissolved in DMSO and diluted 20% v/v in saline—i.p. administration on days 1 and 7; (iii) eight doses of 2 Gy; (iv) eight doses of 2 Gy + CT on days 1 and 7; (v) two doses of 8 Gy; and (vi) two doses of 8 Gy + CT on days 1 and 7. Tumor volume was measured every other day, at least 3 days a week, using the formula:

\[
\text{Tumor volume} = \frac{\text{length} \times \text{width}^2}{2}
\]

**Statistical Analysis**

Statistical analyses were performed by two-way ANOVA with Tukey’s multiple comparisons test using GraphPad Prism (Version 8, USA). Curve fitting of the linear quadratic (LQ) model were performed using SPSS (IBM, Version 25, USA). Values of α and β were derived from the best fit to the survival curves of normoxic and hypoxic condition, from which the
oxygen enhancement ratio (OER) was then calculated using the formula (17):

$$\text{OER} = \frac{\alpha_{\text{hypoxia}}}{\alpha_{\text{normoxia}}}$$ (2)

Detailed experimental information is available in the Supplementary Materials and Methods.

RESULTS

Establishment and Characterization of NPC PDXs

Of 18 NPC patient samples (10 newly diagnosed and 8 recurrent) implanted in NSG mice [mostly subcutaneous (SC) at the flank or both sub-renal (SR) and SC], only five proceeded to passage 1 (P1), showing modest transplantable success rate of 27.8%. Two were lost due to bacterial infections at P2 and P4, and the third could not be maintained beyond P2. The remaining two PDX lines [296T (SC) and 250T (SR)] took about 2.5 and 4 months respectively to be passaged from P0 to P1. While 296T xenografts were propagated every 2 months after P6 and 250T had an average time to propagation of ≈4 months. In an effort to maintain these lines, we revived the slow frozen samples at P3-P5 and achieved stable PDX growth following SC implantation with ≈60% success rate. The detailed clinical information of all 18 donors are listed in Table 1.

Establishment and Characterization of NPC Organoids From PDXs

Representative images of organoid growth and morphology are shown in Figure 1B. Organoids were grown in various commercially available media to fine tune the optimal growth and viability (Figures S1A, B). P-ALI media with optimized NF supported organoid viability for up to 45 days (Figures S1C, D). Organoids could also be cultured from single cell fraction (SCF) that self-assembled to form spheroids (Figures S1E, F), which were then encapsulated in Geltrex (Figure S1G) or re-implanted in animals to establish xenograft tumors (Figure S1H) with similar histopathological features and EBV expression as that of the respective PDX (Figure S1I, J). Histologically, patient tumors, corresponding PDXs, and organoids featured atypical cells with high nuclear/cytoplasmic ratio (Figure 1C).

Transcriptomic Fidelity of PDX and Organoids

RNA-seq analysis of both PDX and organoids revealed a high percentage of reads uniquely mapped to human reference genome (average 82 and 87.1%, Figures 2A–C). Comparison between early (≤P2), intermediate (P3–P10), and late passages (P10–P18) using GSEA showed significantly up-regulated expression of chemokines and inflammatory pathways in
earlier passages of the PDX compared to the intermediate and late passages (Figure 2D). PCA (Figures 2E, F) showed the existence of inter-tumoral differences between the various biopsies and PDX/organoid derivatives along PC2, where the patient tumors were most dispersed. However, the established models (250T and 296T) were well-clustered within the same patient group, while being far apart from each other. The top 100 contributing genes on PC2 suggested the relative differences lied in the extracellular space, keratinization, and epithelial cell differentiation based on g:Profiler analysis (Figure 2G). On comparing the gene expression of the biopsies with the PDX/organoids derivatives using GSEA, we observed significant up-
regulation in metabolism, together with extracellular matrix (ECM) organization and epithelial-mesenchymal transition (EMT) in biopsies, while there was a significant down-regulation of genes related to ribosomal proteins, MYC targets, and oxidative phosphorylation in the derivatives (Figure 2H).

Establishment of Hypoxic Radioresistant NPC Organoids

Organoids were cultured in 1% hypoxic incubator to establish in-vitro hypoxic NPC model. Staining with Green Hypoxia Reagent (GHR) revealed significant hypoxic areas in hypoxic organoids beyond 200 µm in diameter as early as day 4 (Figures 3A and S3A–B). Irradiation of normoxic organoids with a dose of 12 Gy on 3 consecutive days (Figure 3B) led to about 85% reduction in cell viability by 1 week (Figure 3C). In sharp contrast, hypoxic organoids revealed radioresistance and had no significant reduction in end-point cell viability. Staining the organoids with anti-Ki-67 following RT revealed active ~2-fold proliferation of the cells in the peripheral region of the hypoxic organoids, but not in the normoxic organoids (Figures 3D and S3C). QPCR analysis indicated twice the expression of hypoxia inducible factor-1α (HIF-1α) in non-irradiated hypoxic organoids compared to normoxic counterparts, and further ~2 folds increase following RT (Figure 3E). Furthermore, there was a significant γ-H2AX phosphorylation, corresponding to DNA double-strand breaks in normoxic organoids following RT (Figure S3D).

Organoid Models as a Platform to Establish Radiobiological Parameters for NPC

The differences in the radiobiological characteristics and treatment outcomes of normoxic and hypoxic organoids suggested that they have distinct radiobiological parameters. While re-RT could control the proliferation of normoxic areas within recurrent NPC, effective control of radioresistant hypoxic areas might require a larger RT dose. In order to determine the boost in RT dose required by the hypoxic sub-volume, we irradiated organoids, C666-1 spheroids as well as monolayer cultures just once, at doses ranging from 0.5 to 30 Gy (Figure 4A). Changes in cell survival as a function of the dose at day 21 are illustrated (Figure 4B), to determine radiobiological
parameters $\alpha, \beta$ (Table 2) and $\alpha/\beta$ ratio (Figure 4C). Hypoxic NPC organoids displayed a higher $\alpha/\beta$ ratio than that of normoxic ones. The OER, which is the boost in RT dose required to achieve similar biological effect in hypoxic cells as compared to normoxic cells, was found to be about 1.4 for organoids Normoxic and hypoxic C666-1 monolayer had similar $\alpha/\beta$ ratio. However, hypoxic C666-1 spheroids showed $\approx$3 times higher $\alpha/\beta$ ratio compared to normoxic spheroids. Owing to their self-assembly in low-attachment surfaces, spheroids had a larger and non-uniform size compared to organoids, perhaps resulting in a larger hypoxic core when cultured at hypoxic conditions, and thus a higher OER (Figure 4C).

**Hypoxic Organoids Are Less Sensitive to Hyperfractionated RT**

On comparing the effect of RT without and with fractionation (Figure 4D), we found that a single large dose caused significant reduction in cell viability compared to smaller fractionated doses in hypoxic organoids (Figures 4E, F). OER correction further improved the cell killing efficiency of the fractionated dose and resulted in the same amount of cell death in hypoxic organoids as in the normoxic organoids. Hence, hypoxic cells require a large bolus radiation dose, or 1.4 times of the fractionated dose that is effective against normoxic cells.
Hypofractionated RT Results in Substantial Tumor Growth Delay In-Vivo

As NSG mice are extremely sensitive to RT due the PRKDC gene mutation (19), the maximum tolerable whole body irradiation dose is 4 Gy. Targeted irradiation using a custom-made lead shield to irradiate the tumor-site alone, allowed escalation of the dose up to 8 Gy/week. Before irradiation, extend of hypoxia within different sized tumors were analyzed. Even a 200–300 mm³ PDX tumor had considerably large hypoxic areas (Figure 5A). In-vivo treatment (Figure 5B) results revealed that RT with two 8 Gy doses led to significant tumor growth control with 100% survival (Figures 5C–E). While, the addition of CT to this group did not further improve tumor control, it resulted in 50% drop in survival rate by day 29. Addition of CT alongside fractionated RT (2Gy × 8), on the other hand, displayed significant tumor growth control compared to RT alone. However, there was still no survival benefit due to the severe toxicity associated with CT. Besides toxicity, the animals in this group also suffered from paralysis of the left-hind leg, which was the site of irradiation. Staining of the harvested tumors with proliferation marker Ki67, revealed far lesser number of proliferative tumor cells following radiation with 8 Gy × 2 compared to 2 Gy × 8 dose (Figures 5F, G).

Single vs Combined Treatment Modalities

Standard biologically effective dose (BED) model states that biological effect of a dose (d) per fraction (f) given to a tissue in n fractions is given by:

$$\text{BED} = nd \left[ 1 + d \left( \frac{\alpha}{\beta} \right) \right]$$ (3)

where BED is expressed in Gy_{eq \beta} (20). The standard RT dose scheme has been prescribed as a total given dose of 60 Gy in 2 Gy/f, resulting in total BED of 72 Gy_{10}. Conventionally, the prescribed dose for hyper- and hypo-fractionated RT is 1.8 and 4 Gy respectively (17). Taking into account the experimentally determined OER value of 1.4, we propose 2.52 Gy/f for hyperfractionated RT and 5.6 Gy/f for hypofractionated RT.

Table 3 summarizes different RT schemes and their calculated number of fractions for each scheme based on their corresponding BED_{alpha,beta} being close to the standard dose scheme of 72 Gy_{10}.

**DISCUSSION**

Locoregional recurrences in NPC patients may potentially arise from “in-field” radioresistant hypoxic cancer cells that survived the previous course of treatment (21). Hence, more aggressive RT may be required to eliminate these cells, which is practically impossible due to the adverse side effects of re-treatment and the inability to precisely target the GTV while sparing the surrounding critical structures. Lack of accurate models to optimize and personalize re-treatment regimens due to the difficulty in establishing in-vitro and in-vivo patient derived NPC models (22), is another obstacle impeding research progress in the field. For decades, attempts to establish in vitro EBV-positive NPC cell lines have been disappointing, either with the disappearance of all epithelial cells due to the outgrowth of fibroblasts or the emergence of an EBV-negative epithelial cell line after long-term cultures (23). In fact, this lack of EBV was not just due to the loss of the EBV episome, but there is evidence of widespread HeLa contamination in several NPC cell lines such as CNE1, CNE2, AdAH, NPC-KT, and HONE1 (24, 25). Traditionally, NPC cells were cultured by passaging the tumors as xenografts in immunocompromised mice, such as the widely studied C15 tumor, which retains EBV (26). The only NPC cell-line consistently harboring EBV is C666-1 cells, derived from Xeno-666 NPC xenograft derived from an undifferentiated patient tumor (22) and is currently the gold standard used in NPC research. Recently, two more NPC cell-line models carrying EBV were established, which definitely are invaluable tools in NPC research (18, 22).

In the present study, we established two PDX lines and further utilized them to establish in-vitro 3D models of hypoxic radioresistant NPC for the first time. Unlike other cancer types,
NPC biopsy specimens are tiny and insufficient for direct organoid establishment. RNA-seq analysis revealed good correlation between biopsies and corresponding PDXs and organoids, suggesting the suitability of PDX tissues as a sustainable source for organoid establishment. As reported previously (18, 22, 27), take rate of PDX-engraftment was very modest and the two successful lines were both obtained from recurrent NPC patients. Lin et al. reported the possibility of reactivation of lytic EBV during the transplantation of human tissues into immune-suppressed mice (18). Early lytic genes have been detected in a small fraction of NPC patient tumors (28), but a significant upregulation of BZLF-1 in our early PDX and organoids suggests a clonal selection of a sub-population of cells with an abortive lytic reactivation of EBV in early phases of the cultures (29). This may have also resulted in the observed upregulation of host immune and inflammatory reactions, perhaps resulting in tumor cell death and reduced take rate in

**FIGURE 5** | Effect of in-vivo RT. (A) Representative images of immunohistochemical staining of hypoxic regions using Hypoxyprobe and corresponding H&E staining of tumor tissue; magnification 200×, scale bar 200 µm. (B) Schematic of RT regimen with and without CT. (C) Representative images of mice showing the size of PDX (296T) tumors at Day 20 from the start of the treatment. (D) Tumor growth volume measurements from day 0 to 28, n = 7, ns, not significant, *p = 0.0065, **p = 0.0001, ***p < 0.0001. Blue asterisk denotes p values of treatment group vs. untreated control at day 25. (E) Survival curve following the treatment of the animals up to day 30, n = 7. Statistical analysis was performed using the log-rank test, *p < 0.05. (F) Representative images of immunohistochemical staining of Ki67 in the harvested tumor tissue following different treatment, magnification 200×, scale bar 250 µm. (G) Percent area of Ki-67 positive nuclear staining in harvested tumor tissues, n = 3, *p < 0.05, **p < 0.01, ***p < 0.0001. Blue asterisk denotes p values of treatment group vs. untreated control.
TABLE 3 | Tabulation of the proposed photon dose scheme and its calculated BED_{hyp} based on experimental values of α/β ratios and of oxygen enhancement ratio (OER) [Eqn. (3)].

| Dose schemes                  | Hypoxic condition |
|-------------------------------|-------------------|
|                               | Physical dose per fraction (Gy) | Number of fractions | BED_{hyp} (Gy) |
| 1. Conventional photon        | 2                  | 30                  | 72             |
| 2. Hyperfractionated photon   | 2.52               | 25                  | 72             |
| 3. Hypofractionated photon    | 5.6                | 10                  | 74             |

Values of α/β = 10 Gy and OER = 1 were used in the conventional photon dose scheme (1), while α/β = 17.7 Gy and OER = 1.4 were applied to hyperfractionated (2) and hypofractionated (3) dose scheme. BED_{hyp} = 72 Gy is referred as the standard conventional radiotherapy dose scheme in the current study. Physical dose per fraction in hyperfractionated scheme of 1.8 Gy·1.4 = 2.52 Gy and in hypofractionated scheme of 4 Gy·1.4 = 5.6 Gy with α/β = 17.7 Gy were used to calculate the number of fractions with their corresponding BED_{hyp} close to 72 Gy to match the dose scheme with the standard reference dose scheme.

Irradiation of NPC organoids revealed that the hypoxic organoids that mimicked the radioresistant hypoxic sub-volume, required multiple high RT dose before responding to therapy, while the normoxic counterpart seemed to be susceptible to RT. The observed radioresistance was due to the activation of HIF-1α that could trigger multiple downstream signaling pathways leading to proliferation and survival of hypoxic NPC cells (34). The observed differences in radiobiological characteristics and treatment outcomes between normoxic and hypoxic organoids suggest that they have distinct radiobiological parameters. It is interesting to note that hypoxic organoids had higher α/β ratio, indicating that they might be less sensitive to fractionation (35). Whereas, C666-1 monolayer displayed α/β ratio close to the assumed value of 10 Gy. Our in-vitro data comparing fractionated dose with bolus radiation dose, revealed that a modest boost of 40% of the original dose to the normoxic fraction is sufficient to cause significant cell damage to the hypoxic sub-volumes, and these cells were less sensitive to fractionation. As the PDXs were established from patients who failed initial chemoradiotherapy with Cisplatin and Gemcitabine, we added another combination of CT drugs to evaluate its efficacy in-vivo. Although there was some benefit in the addition of CT to the fractionated regimen, the side effects of CT significantly affected the quality of life and survival of the animals. Hence, further studies with a range of fractionated doses with OER correction and equivalent BED on in-vivo models as well as fine-tuning of the chemoRT regimen might be necessary to ascertain the exact dose for translating this to the clinics. Although previous studies have found hypofractionation schemes for re-RT in NPC patients to be generally safe, effective and timesaving (36–38), the number of patients treated with this technique is too small make any definite conclusions.

Intensity modulated radiotherapy therapy (IMRT), together with non-invasive 18F-fluoromisonidazole (18F-MISO) hypoxia imaging, has made dose escalation to hypoxic sub-volumes technically possible. However, achieving this with precision, without affecting the organs at risk remains challenging (39, 40). This has sparked interest in proton therapy that could target high therapeutic radiation dose to the tumor with minimal exit dose (41, 42). Many institutions currently perform IMRT in combination with intensity modulated proton therapy (IMPT) for NPC (43–46), with promising local tumor control and reduction in side effects. Development of dose painting algorithm for dose escalation to hypoxic sub-volumes using combination IMRT and IMPT, could benefit from highly conformal and precise treatment delivery, potentially making this approach a paradigm shift in the re-treatment of recurrent NPC patients.

Taken together, this work highlights the development and characterization of patient derived 3D models of NPC that closely mimics cell-cell interactions, cellular heterogeneity, hypoxia, and radio-resistance. Hence, these models represent a straightforward, yet attractive technology that could complement in-vivo studies for better understanding of the underlying mechanism involved in tissue damage/repair, regeneration and response to therapy. However, the absence of human tumor microenvironment in these models is an inevitable drawback, which to an extent can be overcome by co-culture of the organoids with human immune cells and cancer associated mice. On the other hand, establishment of organoids from PDX was 100% successful. Biologically, the major difference between the patient samples and PDX/organoids may lie in the tumor microenvironment. Strict ECM regulation may be lost during establishment of organoids from PDX was applied in the current study. Physical dose per fraction in hyperfractionated scheme of 1.8 Gy·1.4 = 2.52 Gy and in hypofractionated scheme of 4 Gy·1.4 = 5.6 Gy with α/β = 17.7 Gy were used to calculate the number of fractions with their corresponding BED_{hyp} close to 72 Gy to match the dose scheme with the standard reference dose scheme.

The gap between the observed radiation dose, revealed that a modest boost of 40% of the original dose to the normoxic fraction is sufficient to cause significant cell damage to the hypoxic sub-volumes, and these cells were less sensitive to fractionation. As the PDXs were established from patients who failed initial chemoradiotherapy with Cisplatin and Gemcitabine, we added another combination of CT drugs to evaluate its efficacy in-vivo. Although there was some benefit in the addition of CT to the fractionated regimen, the side effects of CT significantly affected the quality of life and survival of the animals. Hence, further studies with a range of fractionated doses with OER correction and equivalent BED on in-vivo models as well as fine-tuning of the chemoRT regimen might be necessary to ascertain the exact dose for translating this to the clinics. Although previous studies have found hypofractionation schemes for re-RT in NPC patients to be generally safe, effective and timesaving (36–38), the number of patients treated with this technique is too small make any definite conclusions.

Intensity modulated radiotherapy therapy (IMRT), together with non-invasive 18F-fluoromisonidazole (18F-MISO) hypoxia imaging, has made dose escalation to hypoxic sub-volumes technically possible. However, achieving this with precision, without affecting the organs at risk remains challenging (39, 40). This has sparked interest in proton therapy that could target high therapeutic radiation dose to the tumor with minimal exit dose (41, 42). Many institutions currently perform IMRT in combination with intensity modulated proton therapy (IMPT) for NPC (43–46), with promising local tumor control and reduction in side effects. Development of dose painting algorithm for dose escalation to hypoxic sub-volumes using combination IMRT and IMPT, could benefit from highly conformal and precise treatment delivery, potentially making this approach a paradigm shift in the re-treatment of recurrent NPC patients.

Taken together, this work highlights the development and characterization of patient derived 3D models of NPC that closely mimics cell-cell interactions, cellular heterogeneity, hypoxia, and radio-resistance. Hence, these models represent a straightforward, yet attractive technology that could complement in-vivo studies for better understanding of the underlying mechanism involved in tissue damage/repair, regeneration and response to therapy. However, the absence of human tumor microenvironment in these models is an inevitable drawback, which to an extent can be overcome by co-culture of the organoids with human immune cells and cancer associated.
fibroblasts. We further utilized the 3D models together with simple dose-survival data analytic techniques to yield quantitative readouts that defines the inherent radiobiological characteristic of radiosensitive normoxic and radioresistant hypoxic NPC. With combined experimental data, we conclude that hypoxic NPC require a large bolus dose or 1.4 times of the fractionated dose that is effective against normoxic cells in order to compensate for oxygen shortage. Further clinical results should be obtained in order to confirm its usefulness and translational value. In conclusion, this study could be a game changer in the way such models are utilized for optimization of radiation dose and our findings may have profound implications on how radiation treatments are planned in future, especially for re-irradiation of recurrent NPC.

DATA AVAILABILITY STATEMENT

The datasets presented in this study can be found in online repositories. The names of the repository/repositories and accession number(s) can be found below: NCBI Gene Expression Omnibus (https://www.ncbi.nlm.nih.gov/geo/query/acc.cgi?acc=GSE164544).

ETHICS STATEMENT

Patient specimen collection and experimental use were approved by the institutional review board of National Healthcare Group (DSRB Reference: 2015/00098-SRF00004). The participants provided their written informed consent to participate in this study. All animal care and experimental procedures were approved by the Institutional Animal Care and Use Committee, A*Star Research Entities, Singapore.

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AUTHOR CONTRIBUTIONS

MT and SL conceived and designed the experiments. CL provided patient samples. SL performed the experiments. JS helped with establishment of PDX animal model. JM, MHL, and JW helped with RNA sequencing data analysis. ML, SY, DY, and SD analyzed dose-survival data. SL wrote the manuscript and performed literature, with the help of ML. All authors contributed to the article and approved the submitted version.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fonc.2021.622244/full#supplementary-material

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Conflict of Interest: ML, SY, DY, and SD were employed by the Proton Therapy Centre Pte. Ltd.

The remaining authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.