The widely used SPECT and PET tracers for cardiac sympathetic nervous system

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Abstract

Dysfunction of the cardiac nervous system implicated in various types of cardiac disease has been recognized. With the development of single photon emission computed tomography (SPECT) and positron emission tomography (PET), nuclear imaging technique make it possible for global and regional investigation of the myocardial sympathetic nervous system. The SPECT tracer 123I-metaiodobenzylguanidine (123I-MIBG) has been applied for mapping pre-synaptic sympathetic innervation and is available for imaging on various heart diseases now. PET tracer 11C-meta-hydroxyephedrine (11C-HED) has also been established for characterizing the cardiac sympathetic nervous system. And the PET tracer LMI1195, which is under clinical investigation, is a promising tracer.

Abbreviations: SPECT: single photon emission computed tomography, PET: positron emission tomography, DOPA: dihydroxyphenylalanine, MOA: monoamine oxidase, MIBG: metaiodobenzylguanidine, CAD: coronary artery disease

Cardiac sympathetic nervous system

The cardiac nervous system was divided into two portions: sympathetic and parasympathetic innervation. Among the cardiac nervous system, the sympathetic nervous system is the critical autonomic component in the ventricles, whereas parasympathetic nerve fibers are primary in the atria and less abundant in ventricular myocardium. Autonomic nerves travel along coronary vascular structures and go into underlying myocardium. NE concentration shows a gradient in sympathetic innervation from the base to the apex of the heart [1,2]. Norepinephrine and acetylcholine are their major neurotransmitters respectively, which binding to adrenergic receptors and muscarinic or neuronal nicotinic receptors at target cardiac tissue. The two neurotransmitters exert stimulating or inhibitory effects on cardiac inotropy and chronotropy (force of contraction, heart rate and conduction) via adrenergic and muscarinic receptors to adapt to changing cardiovascular demand. In all, the cardiac neuronal network exerts a reciprocal, concerted action plays an important role in the performance of cardiovascular system. The pathophysiology of cardiac disease is attributed to the dysfunction of the cardiac nervous system.

In neuronal vesicles, tyrosine is converted to dihydroxyphenylalanine (DOPA), then with the help of DOPA-decarboxylase, the DOPA is further converted to dopamine. Dopamine β-hydroxylase catalyzes the dopamine into NE. Some NE is further transformed to epinephrine by phenylethanolamine-N-methyltransferase [3]. And choline acetyltransferase catalyzes the choline and acetyl-CoA into ACh. Then, the release of NE and ACh into synaptic cleft is mainly regulated by sympathetic nerve and parasympathetic nerve respectively. The NE uptake transporter (uptake-1) could return synaptic NE to the neuronal cytosol for packaging into vesicles or degradation by monoamine oxidase (MAO) and catechol-O-methyltransferase, as the cocaine and desipramine could pharmacologically blocked the process [4-6]. Furthermore, more researches show that uptake-1 system density is highest in the left ventricle, less abundant in right ventricle and atrial tissue [7]. Only a small part of synaptic NE is subject to postsynaptic transport via the uptake-2 pathway (Figure 1) [8,9]. And a small proportion of the released norepinephrine also diffuses into vascular space [10]. Choline is recovered into the neuron to be reincorporated into ACh after ACh in the synapse is broken down by the acetycholinesterase.

123I-metaiodobenzylguanidine (MIBG)

123I-metaiodobenzylguanidine(MIBG), as a single-photon emission computed tomography (SPECT) tracer, acts selectively on sympathetic nerve ending, that is an analogue of the antihypertensive drug guanethidine (Table 1) [11]. MIBG has been developed as the most widely used nuclear tracer for studying cardiac sympathetic activity in various of cardiac diseases. As a false neurotransmitter, MIBG is not metabolised by MAO or COMT, which allow it to be a nuclear tracer [12,13]. The uptake-1 mechanism is responsible for transporting MIBG into neurons, so it also play a important role in the MIBG uptake. In addition to uptake-1 mechanism, the uptake-2 system removes MIBG into nonneuronal tissue [14-16]. It has been reported that the clearance of MIBG from the extraneuronal compartment is much faster than clearance from the neuronal tissues [15,16]. So MIBG uptake is not observed in denervated myocardium in transplanted heart [17].

After intravenous injection of 111 to 370 MBq (3 to 10 mCi) 123I-MIBG, early (15 to 30 min) and late(3 to 4 h) SPECT images obtained following the imaging protocol. By calculating a heart-to-
mediastinum ratio (HMR) after drawing regions of interest over the heart and mediastinum, the heart MIBG uptake is semi-quantified [18]. And by comparing early and delayed activities, the wash-out (WO) rate can be gained, which reflecting retention of NE by sympathetic neurons (Figure 2) [19]. Polar maps constructed from the SPECT images can evaluate the regional sympathetic activity. Differences between regional innervations and perfusion can be measured by comparing 123I-MIBG SPECT images with SPECT myocardial perfusion images [20,21]. Above all 123I-MIBG has been widely applied in cardiac diseases such as coronary artery diseases, myocardial infarction and heart failure.

**11C-Hydroxyephedrine**

For the imaging of cardiac sympathetic neurons, the most widely used PET tracer is 11C-meta-hydroxyephedrine (HED). It is reliably synthesized in high specific activities by N-methylation of the NE analogue metaraminol (Table 1). HED is resistant to metabolism by MAO or catechol-O-methyltransferase and transports through uptake-1 system [22]. Research in isolated perfused rat hearts after desipramine blockade and denervated human hearts demonstrated that nonspecific myocardial HED uptake is low [23,24]. Although vesicular storage seems to occur, binding inside vesicles is reduced because of a higher lipophilicity of HED compared with norepinephrine [25]. The cardiac HED retention index is largely relying on the norepinephrine transporter reuptake. When the additional desipramine or norepinephrine was added to the perfusate after use of HED in isolated rat hearts, the rat heart HED washout was accelerated. This phenomenon suggests that continuous release and reuptake of HED by sympathetic neurons is thus believed to undergoing [23]. With endogenous and exogenous catecholamines in isolated perfused rat hearts and in vivo in mice and humans, increased rate of tracer washout has been observed because of the competition for the uptake-1 system [26-29]. Treating with the VMAT inhibitor reserpine, the partial packaging of 11C-HED into vesicles by reducing tracer uptake was seen in dogs and rabbits researches [30].

Quantification of 11C-HED uptake is routinely reported as a retention index, a ratio of activity in the myocardium in the final image of a 40 or 60 minutes dynamic sequence to the integral of the image-derived arterial blood time activity curve [23,31]. As lower uptake of 123I-MIBG was seen in the posterior inferior wall, distribution of HED throughout left ventricular myocardium in healthy normal individuals is consistent with other myocardial segments [24]. The retention of 11C-HED, therefore, could reflect the whole spectrum of presynaptic activity, including uptake-1 system, vesicular packaging, and vesicular release.

### Coronary heart disease

One of the primary clinical applications of sympathetic neuronal tracers was in the evaluation of patients with coronary artery disease. Compared with myocardial tissue, the sympathetic neuronal tissue is more easily damaged by the ischemia [32]. In patients with stable coronary artery disease without previous myocardial infarction, the reduction of MIBG uptake can be detected [33]. Research shows that the size of the MIBG defect was associated with severity of coronary stenoses, which demonstrated that cardiac adrenergic tissue is very sensitive to the damage caused by ischemia. In this study, the MIBG defect is significantly larger than MIBI defect when patients at rest and during exercise, which proves that the cardiac nerves is more vulnerable to the ischemia than the myocardial tissue [34]. But in another study, the overall diagnostic accuracy of late MIBG scanning was 66% and the positive and negative predictive values and kappa value were low; 60%, 70%, and 0.31, respectively [34]. Nonspecific reductions of MIBG uptake in the inferior and posterolateral regions restricted the diagnostic accuracy of MIBG tomography in coronary artery disease [34]. Researches show that although myocardial perfusion could be improved after 6 months exercise rehabilitation in patients with ischaemic heart disease, the size of innervation defects of myocardium could not show significant differences [35]. And 123I-MIBG could also be used for the examination of the patients incapable of exercising. Under normal circumstances, the perfusion imaging combined with pharmacological stress is a choice. However, some particular medical condition does not allow the use of pharmacological stress. Under the circumstances, resting imaging with 123I-MIBGcombined with resting myocardial perfusion imaging (MPI) may be useful as a sign of reversible ischemia [35].

In patients after AMI, regional cardiac MIBG uptake in the region of infarction is significantly reduced. In all patients, the area of reduced MIBG uptake after 4 hours was more extensive than MIBG perfusion defect. And left ventricular ejection fraction correlated with the 4-hour MIBG defect score [36].

For the PET tracer 11C-HED, the results of coronary artery disease are similar. In patients with coronary artery disease (CAD) without myocardial infarction, quantifiable 11C-HED and high resolution of PET could identify regional alterations in sympathetic innervation with normal resting perfusion. As to myocardial reinnervation after regional ischemic, the same to the MIBG, HED uptake of the myocardium is nearly unchanged in both diabetic and nondiabetic patients with stable...
chronic coronary artery disease in a 1-y follow-up [37]. These researches further supported the hypothesis of a higher sensitivity of sympathetic neurons to ischemia compared with cardiomyocytes [38]. As to the patients with an acute myocardial infarction, 11C-hydroxyephedrine abnormalities were also more extensive than those for blood flow assessed by semiquantitative polar map analysis (Figure 3), especially in five patients with non-Q wave infarction [39]. And no change was also observed in regional reduction of HED uptake until 6 months after acute infarction, which demonstrated that there is no evidence of reinnervation of the injured myocardium [39]. In an animal study, to generate hibernating myocardium, pigs were underwent coronary artery restriction at the proximal left anterior descending artery. As a result, although significant functional improvement of hibernating myocardium owing to PCI or pravastatin therapy, no changes in HED defect size or severity was observed [40].

**Heart failure and cardiac mortality**

Cardiac remodeling is a hallmark among the development of cardiomyopathy and heart failure, which could result in the damage of sympathetic neurons. Enhanced 123I-MIBG washout rate and delayed but not early heart-to-mediastinal ratio (late HMR <1.74) can be observed in the patients with non-ischemic cardiomyopathy [41]. Also, the 11C-HED uptake permeability was significantly reduced among congestive heart failure patients (LVEF<45%) [42]. Regional defects of 11C-HED retention have been correlated with impaired contractile function and left ventricular ejection fraction, but not directly with oxidative metabolism [43-45]. Another research further demonstrate that depressed heart rate variability and baroreflex sensitivity, which consistent with impaired autonomic neuronal function, also has a close relationship with the reduction of 11C-HED in failing hearts [46].

123I-MIBG imaging has showed that abnormalities in global cardiac innervation could be a sign for cardiac mortality in patients with heart failure. A study including 112 heart failure patients with a poor LV function shows impaired cardiac sympathetic innervation imaged with 123I-MIBG correlated with poor prognosis. More research shows 123I-MIBG is the independent predictor for mortality, and compared with patients with reduced 123I-MIBG, patients with normal 123I-MIBG showed a 2-year event-free survival [41,47]. As to 11C-HED, the researches of PET imaging in chronic heart failure also shows that 11C-HED PET also provides independent prognostic information in patients with CHF [43].

**Arrhythmias**

Abnormalities in the autonomic nervous system have led to ventricular arrhythmias [48,49]. As cardiac sympathetic denervation has a close relationship with ventricular arrhythmias, sympathetic nerve imaging with 123I-MIBG could be used for predicting the occurrence of arrhythmias after myocardial infarction [50]. A pilot study that 17 patients suffering from sustained ventricular tachycardia or ventricular fibrillation treated with ICD showed apparently more global (early H/M ratio) and regional sympathetic denervation (early and late 123I-mIBG defect score) than patients without an ICD discharge (Figure 4) [51]. And advanced study demonstrated that late 123I-MIBG SPECT reflecting the regional cardiac sympathetic denervation was significantly correlated with ventricular arrhythmias needing appropriate ICD therapy. Moreover, late 123I-MIBG SPECT defect score could be an independent indicator for appropriate ICD therapy, but myocardial washout rate was not predictive for appropriate ICD therapy [52].

![Figure 2. Calculation of Cardiac mIBG Activity. (A) mIBG heart-to-mediastinum ratio (HMR) and wash-out rate were calculated on an anterior view. (B) Normal cardiac mIBG activity, a typical low-risk patient, with HMR: 1.70. (C) Severely decreased cardiac mIBG activity, a typical high-risk patient, with HMR: 1.10.](image-url)
Also abnormal patterns of $^{11}$C-HED retention were studied in right ventricular tachycardic arrhythmias. Patients with idiopathic right ventricular outflow tract tachycardia (RVO-VT) showed myocardial reduced HED uptake compared with the control subjects [53,54]. And in Brugada syndrome, compared with a group of age-matched healthy control subjects, the $^{11}$C-HED uptake, which representing presynaptic sympathetic norepinephrine recycling, was apparently increased in patients with Brugada syndrome [55]. In another study to evaluate cardiac sympathetic innervation with $^{11}$C-HED PET in genotyped LQTS patients, results show that decreased $^{11}$C-HED retention was seen in most LQTS patients [56].

**Parkinson disease**

As we all know that idiopathic Parkinson disease (IPD) is associated with multiple autonomic morbidities, including cardiac postganglionic and presynaptic sympathetic denervation. The PD patients imaged with $^{123}$I-MIBG demonstrate that cardiac sympathetic denervation is common. And the phenomenon seems to occur independent of the clinical stage and symptoms in patients with IPD, as the mean plasma adrenaline and noradrenaline levels are still in the normal level [57]. Cardiac sympathetic denervation imaged with $^{123}$I-MIBG has been proposed as a diagnostic test with which to differentiate IPD with postganglionic autonomic dysfunction from other Parkinsonian syndromes such as multiple system atrophy with central and preganglionic sympathetic dysfunction (Figure 5). In this research, significant positive relationship between cardiac MIBG uptake and the Cross-Cultural Smell Identification (CCSI) score in patients with PD could be found, whereas patients with MSA does not show significant correlation [58,59]. Primary progressive Freezing Gait (PPFG) also needs to distinguish with the Parkinson's Disease, because Freezing of gait (FOG) is a late manifestation of Parkinson's Disease. Results demonstrate that patients with PPFG show no reduction of cardiac MIBG uptake which could help distinguish patients with PPFG from those with PD and early FOG [60].

As cardiac PET is more sensitive and accurate than the SPECT, $^{11}$C-HED PET image is also used to reflect sympathetic nerve density

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**Figure 3.** In a patient 3 weeks after nontransmural infarction of the distal left anterior descending artery territory. Mismatch of myocardial perfusion, as measured by nitrogen 13 ammonia ($NH_3$), and innervation, as measured by C-11 hydroxyephedrine ($HED$).

**Figure 4.** Example of Resting Myocardial Perfusion (A) and Late 123-I MIBG Imaging (B) in an ICD Patient.
in PD patients. Compared with $^{123}$I-MIBG image, another research with the use of image with $^{11}$C HED demonstrate that extensive cardiac denervation was observed in several patients with IPD [61,62]. However, among some patients with MSA and PSP, we could also observe the substantial cardiac denervation [62]. Furthermore whether cardiac sympathetic denervation in IPD influences the left ventricle in a distinct regional pattern versus a more global pattern with application of $^{11}$C-HED PET was put into research. Results show that cardiac sympathetic denervation is extensive in IPD and affects most patients at an early stage in the disease course. The part of cardiac sympathetic denervation involves the proximal lateral left ventricular wall most severely, with relative sparing of the anterior and proximal septal walls [63].

$^{18}$F-LMI1195

$^{18}$F-LMI1195($^{18}$F-N-[3-bromo-4-(3-fluoro-propoxy)-benzyl]-guanidine) is a new PET tracer which is designed for imaging of cardiac sympathetic innervation. $^{18}$F-LMI1195 can be synthesized by a single-step nucleophilic substitution reaction, followed by a high performance liquid chromatography purification with a high radiochemical yield [64]. Although the $^{11}$C-HED and other PET tracers make it possible for assessment of cardiovascular sympathetic system abnormalities, the limitation of short half-life of $^{11}$C (20 min) reduces its clinical application because of the need for a costly on-site cyclotron [65]. So the $^{18}$F-LMI1195, a newly 18F-labeled PET imaging tracer has been developed to overcome these shortness of the PET tracers [64]. A longer physical half-life (110 min) of 18F-radionuclides, allowing for delayed or prolonged imaging and more research plan. The in vitro assays showed that LMI1195 had a cell uptake profile similar to NE, comparable NET binding affinity and NET-mediated cell uptake kinetics [64].

The initial evaluation of this novel tracer was performed in cells and animal models. The uptake ratios of heart to adjacent organs such as blood, lung, and liver for LMI1195 were high in rabbits and higher than for $^{123}$I-MIBG in rats. In contrast to the high and sustained $^{123}$I-MIBG liver retention, these findings suggest that cardiac images of LMI1195 should have less interference by the background activity in organs such as the liver [64]. As discussed before, $^{11}$C-hydroxyephedrine cardiac retention is maintained by continuous reuptake via NET and release from the nerve terminals, further research show that $^{18}$F-LMI1195, analogous to $^{123}$I-MIBG, demonstrated stable tracer retention resistant to the NET inhibitor chase treatment, whereas $^{11}$C-hydroxyephedrine cardiac retention is maintained by continuous reuptake via NET and release (diffusion) from the nerve terminals [66]. In rats, phenoxybenzamine but not desipramine could significantly inhibit cardiac uptake of $^{18}$F-LMI1195, proving that 18F-LMI1195 is a substrate for the uptake-2 mechanism and is consistent with the rat heart having a dominant level of the mechanism [67]. Also the first-in-human study of the 18F-Labeled Tracer was conducted in 2014. 150-250 MBq of LMI1195 were injected intravenously into twelve healthy subjects at 3 clinical sites. Then dynamic PET images were get over the heart for 10 min, followed by sequential whole-body images for nearly 5 h. No adverse events due to LMI1195 were found during the 5h. Blood radioactivity cleared quickly, whereas myocardial uptake remained stable and uniform throughout the heart over 4 h. Favorable target-to-background ratios for cardiac imaging was obtained owing to rapidly clearance of liver and lung activity [68].

Impaired NET function in the heart has been identified in heart failure of animals and humans with different reasons including hypertrophy, valvular and ischemic heart disease and idiopathic hypertrophic cardiomyopathy [69-71]. Therefore, measuring cardiac NET function may be useful for monitoring the disease progression and cardiac events in patients with HF. Imaging in these DSS rats showed reduced LMI1195 heart uptake following progression of HF development, as MIBG uptake was normal at the myocardial hypertrophy stage of DSS rats, even though the heart NE content decreased [72].

Regional cardiac sympathetic denervation (RCSD) associated with reduced noradrenaline transporter (NAT) function has been related to cardiac arrhythmia. LMI1195 cardiac imaging was applied for imaging of RCSD in a rabbit model surgically developed by regional phenol application on the left ventricular (LV) wall. So LMI1195 shows a close relationship with NAT and can be used for imaging RCSD [73].

As a promising PET nuclear tracer, the more clinical uses of LMI1195 in cardiac diseases need to be deeply studied. Advantages and disadvantages of LMI1195, compared with other PET tracers, also wait to be illustrated by researchers.

**Conclusion**

$^{123}$I-MIBG and $^{11}$C-HED imaging provides a noninvasive tool for the investigation of cardiac sympathetic innervations which could be used for the assessments of various of cardiac diseases and Parkinson disease. As the sympathetic neuronal tissue is more easily damaged compared with the myocardium, so the $^{123}$I-MIBG and $^{11}$C-HED imaging is more sensitive than other examinations. But they are not commonly applied in patients with cardiac diseases or Parkinson disease. More clinical knowledge about cardiac sympathetic nervous system imaging needs further researches that define the prognostic importance of cardiac neuro imaging in various diseases. This may promote the licensure and deployment of neuronal imaging agents for routine use in the clinical setting.
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Disclosure
The authors report no conflicts of interest.

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