Compressed Lateral and anteroposterior Anatomical Systematic Sequences «CLASS»: compressed MRI sequences with assessed anatomical femoral and tibial ACL’s footprints, a feasibility study

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Abstract
Purpose: This study’s main objective is to assess the feasibility of processing the MRI information with identified ACL-footprints into 2D-images similar to a conventional anteroposterior and lateral X-Ray image of the knee. The secondary aim is to conduct specific measurements to assess the reliability and reproducibility. This study is a proof of concept of this technique.

Methods: Five anonymised MRIs of a right knee were analysed. A orthopaedic knee surgeon performed the footprints identification. An ad-hoc software allowed a volumetric 3D image projection on a 2D anteroposterior and lateral view. The previously defined anatomical femoral and tibial footprints were precisely identified on these views. Several parameters were measured (e.g. coronal and sagittal ratio of tibial footprint, sagittal ratio of femoral footprint, femoral intercondylar notch roof angle, proximal tibial slope and others). The intraclass correlation coefficient (ICCs), including 95% confidence intervals (CIs), has been calculated to assess intraobserver reproducibility and interobserver reliability.

Results: Five MRI scans of a right knee have been assessed (three females, two males, mean age of 30.8 years old). Five 2D-”CLASS” have been created. The measured parameters showed a "substantial" to "almost perfect" reproducibility and an "almost perfect" reliability.

Conclusion: This study confirmed the possibility of generating "CLASS" with the localised centroid of the femoral and tibial ACL footprints from a 3D volumetric model. "CLASS" also showed that these footprints were easily identified on standard anteroposterior and lateral X-Ray views of the same patient, thus allowing an individual identification of the anatomical femoral and tibial ACL’s footprints.

Level of evidence: Level IV diagnostic study
Keywords: Knee, ACL footprints, MRI

Introduction
Anterior cruciate ligament (ACL) lesion incidence is about 0.8 per 100,000 people [7, 16]. ACL reconstruction does not prevent the early onset of osteoarthritis in the long term. Still, it can improve knee kinematic and...
can reduce the risk of secondary injury to cartilage and meniscus [8]. The outcome of ACL-reconstruction is dependent on careful selection of footprints [4, 10, 25]. The current recommendations tend to recreate the anatomic rather than isometric footprints [27]. Different options have been described in the literature for proper assessment of femoral and tibial ACL-footprint [12, 19]. Three-dimensional MRI studies showed its reliability [3, 11, 21, 24, 26]. Research has shown that ACL footprints may present a variable location in different individuals [22], and therefore, their intraoperative identification can be challenging. Intraoperative fluoroscopy can help to be more accurate to confirm a proper tunnel placement [14, 20]. However, fluoroscopy alone does not incorporate the footprints' individual anatomical variability. A 2D preoperative (anteroposterior and lateral) construct showing the individual footprints would be needed and act as a model during surgery and fluoroscopic verification of optimal tunnel placement to fill this lack of information.

As most patients who suffer from an ACL tear undergo an MRI scan, we intended to use this image acquisition to create a specific 2D model. This study's main objective is (1) to assess the feasibility of converting MRI information of the ACL-footprints into a 2D image similar to a conventional anteroposterior and lateral X-Ray image of the knee. The secondary aim is (2) to perform specific morphometric measurements. This study is a proof of concept of the technique.

**Material & methods**

Five anonymised MRIs of a right knee were analyzed. None of those showed meniscal, cartilage or ligamentous lesion. Patients had no history of fracture or previous surgery of the knee joint. The growth plates were closed, and there was no skeletal dysplasia or osteoarthritis.

**Compressed Lateral and Anteroposterior Anatomical Systematic Sequence ("CLASS")**

The same standard MR-technique using an Optima MR360 1.5 T Advance scan, GE Healthcare was applied in all cases. All radiographic images were digitally acquired using a picture archiving and communication system (PACS, GE Healthcare, Belgium). The sequences included sagittal proton density fat saturated isotropic 3D with isovoxel of 0.6 × 0.6 × 0.6 mm.

A senior orthopaedic knee surgeon performed the footprint identification using the multiplanar reformation tool of the software Materialise Mimics® 17.0 research. First, the femoral ACL's footprint was identified in the axial view to match the sagittal orientation towards the lateral wall of the notch. The sagittal orientation was then matched to it in the coronal view as well. Finally, the coronal orientation was aligned with the fibers of the ACL in the sagittal view. The femoral footprint was then marked from four points as follow: shallow, deep, high and low (Fig. 1). To identify the tibial ACL's footprint, the sagittal orientation was kept aligned with the fibers of the ACL. The axial orientation was then matched to the tibial joint line in the coronal view. Finally, the axial orientation was aligned with the tibial slope between the tibial spines. The tibial footprint was then identified from four points as follow: anterior, posterior, medial and lateral (Fig. 2). All points were selected at their maximal margins. The previously mapped four points were computed by coordinate averaging with an in-house routine GNU Octave (version 4.0.0) to generate a centroid femoral and tibial optimised footprint. The fibular head's styloid process acting as a reference was identified with a single point. The in-house GNU Octave scripts computed the centroid points' position on the 2D-image reference system and the pixel intensity by averaging the pixel intensity values along the projection direction. By projecting the MRI volumetric image and the calculated points on the lateral and anteroposterior views, the "CLASS" MRI sequence was established.

**Radiographic evaluation**

Using the software ImageJ, several measurements have been performed on the CLASS [23]. On the anteroposterior (AP) view, the location of the ACL tibial footprint...
was established ("coronal ratio tibial footprint"). The sagittal location of the ACL tibial footprint was determined by applying the reference line described by Amis and Jakob [1] ("sagittal ratio tibial footprint") on the lateral (LAT) view. The sagittal location of the ACL femoral footprint was determined by using the reference line described by Amis and Zavras [2] ("sagittal ratio femoral footprint high to low" and "sagittal ratio femoral footprint deep to shallow") on the lateral view as well. The femoral intercondylar notch roof angle ("α") on the lateral sequence was determined using the longitudinal axis of the femur and the Blumensaat line. Two circles were drawn, one tangent to the Blumensaat line and the anterior and posterior femur edges and the other tangent to the proximal border of the distal circle, anterior and posterior femur edges. The longitudinal femoral axis was then assessed by connecting the centres of both circles (Fig. 3). The proximal tibial slope ("β") was measured using the longitudinal tibial axis according to Lipp [15] and the articular surface (Fig. 3). The angle between the tibial articular surface and the ACL footprints was calculated from both the anteroposterior and lateral images ("coronal articular surface and ACL—angle" and "sagittal articular surface and ACL—angle"). On the lateral sequence, the angle between the tibial articular surface and the Blumensaat’s line was measured ("sagittal articular surface and Blumensaat’s line—angle").

The image analysis and angles measurements have been performed independently from each other at two different time frames with a 3-weeks interval. Patients’ names and identifying features were blinded to minimise recall bias. To assess the intraobserver reproducibility and interobserver reliability, intraclass correlation coefficient (ICCs) was calculated including 95% confidence intervals (CIs) based on a mean-rating (k = 2), absolute agreement, 2-way mixed-effects model. The ICC was graded as ICC < 0.20 for slight; 0.21 to 0.40 for fair; 0.41 to 0.60 for moderate; 0.61 to 0.80 for substantial; and > 0.80 for almost perfect agreement [17]. Descriptive analysis has been performed using IBM SPSS Version 26.0 (SPSS Inc, Chicago, IL). The study was carried out following the World Medical Association Declaration of Helsinki. According to federal law, our project did not need the approval of the local ethical committee (http://www.cer-vd.ch/soumission/premiers-pas.html).

Results

Five MRIs of a right knee have been assessed (three females and two males, mean age of 30.8 years old). The Figs. 4 and 5 show the conventional radiogram of a right knee (AP and LAT views). Fig. 6 and 7 show the 2D-compressed anteroposterior and lateral views. Table 1 shows the results of the measurements mentioned above and performed on the newly acquired "CLASS" views.
Discussion
This study’s main objective was to evaluate the feasibility to create 2D-images mimicking an anteroposterior and lateral conventional X-ray expressing precisely the location of the tibial and femoral ACL footprints based on a standard MRI acquisition of a knee. Secondary aims consisted of evaluating the possibility of conducting different measurements used in standard knee radiographic analysis. The intrarater reproducibility and reliability were for all measurements almost perfect, according to Montgomery [17]. Amis and Zavras [2] presented their review on “isometricity and graft placement during anterior cruciate ligament reconstruction”. Based on the illustrated basic principles of isometry and the results found in the literature, they concluded a “close to isometric” zone to be the preferred choice for femoral tunnel placement, and suggested placement at 20% high to low (HL) and 38% deep to shallow (DS) based on the quadrant method. Bernard and Hertel [5] performed an anatomical footprint analysis on 10 cadaveric knees based on the same method. According to their results, the center of the anatomic femoral ACL insertion was located at 28.5% HL and at 24.8% DS. Piefer J.W. et al. [19] did a systematic review on evaluation of the anatomic femoral ACL-footprint and presented a mean value of 35.2% HL and 28.5% DS. Parkar et al. [18] performed a systematic review regarding anatomic location centers of the femoral and tibial ACL footprints and calculated the weighted median of the ACL femoral insertion center to be 34% and 26% in the HL and DS directions, respectively. The 5th and 95th percentiles were 28% and 43%, respectively, for HL, and 24% and 37%, respectively, for DS. Iriuchishima et al.[13] did a systematic study on the performed methods and tunnel placement strategies in anatomical single-bundle ACL reconstruction. Evaluation of 19 studies showed a targeted femoral footprint center at 32.3±7% HL and at 30.6±4.3% DS. Our results showed a mean centroid femoral footprint at 22.2% HL and 37.0% DS in a young and healthy population. Byrne et al. [6] performed a retrospective study to assess femoral tunnel position on routine postoperative radiographs in patients who required ACL revision compared with patients who did not require revision. In patients who did not require revision, the femoral tunnel was 38%±9% HL and 28%±6%
DS. It was shown that too anterior and too high femoral tunnel placement were independent risk factors for ACL revision surgery. It should be noted that in this study, tunnel position was analyzed using only postoperative radiographs. However, the reasons for failed ACL reconstruction may be multifactorial and should be correlated accordingly, as also emphasized in this publication.

Our results showed a mean centroid femoral footprint at 22.2% HL and 37.0% DS in a young and healthy population, and appears to be closer to the isometric footprint suggested by Amis and Zavras [2] than to the median of the systematic reviews. The wide range in the determined anatomical femoral footprint in the literature suggests that this should be correlated with the tibial footprint and other morphological criteria to gain a better understanding. Amis and Jakob [1] described the anatomical tibial ACL-centre as 43% anteroposterior in the lateral standard X-Ray view. Others authors showed similar results with a range of 40 – 46.2% [9]. This variation suggests a patient dependent anatomical ACL-centers. Our result of 42.9% (40.5 – 44.1%) is comparable for this small series of patients [9]. This method’s strength is that the MRI information is not altered to create the 2D-compressed images. The MRI-slices keep most of the MRI information enriched with the ACL femoral and tibial footprints’ location. According to the exclusion criteria, all knees did not show any pathologies. There are some limitations to this study. As the sample size was rather small, further studies using these 2D-compressed images with a larger collective are needed. Its major strength is that this sequence may give a better understanding of the anatomical femoral and tibial ACL’s footprints. This would allow an individual approach for tunnel placement in ACL reconstruction surgery to assess the anatomical variation of the ACL anatomy among the population. Therefore, it could be used as a template during surgery for tunnel placement under fluoroscopic control, for postoperative evaluation of tunnel placement, or as input data for fluoroscopy-based navigation systems.

**Conclusion**

This study confirmed the possibility to compress the information of a 2D/3D-MRI scan of a knee with individually localised tibial and femoral footprints into a “Compressed Lateral and Anteroposterior Anatomical Systematic Sequence”. Specific morphometric measurements can be performed using the newly generated sequences, giving the possibility for individual...
Blumensaat’s line—angle sagittal articular surface and ACL—angle sagittal articular surface and coronal articular surface and 

β 86.967° (86.129 – 87.579) 0.922 with CI 95% (0.234 – 

α 34.243° (31.488 – 35.393) 0.934 with CI 95% (0.005 – 

print deep to shallow sagittal ratio femoral foot‑ 

sagittal ratio femoral foot‑ 

sagittal ratio tibial footprint 0.429 (0.405 – 0.441) 0.816 with CI 95% (‑0.213 – 

coronal ratio tibial footprint 0.506 (0.501 – 0.512) 0.827 with CI 95% (‑0.204 – 

Age (years) 30.8 (29 – 33) n/a n/a n/a

Table 1 Intra and interobserver measurement results

| N = 5 | Mean | Reproducibility (ICC reader 1) | Reproducibility (ICC reader 2) | Reliability (ICC reader 1 versus reader 2) |
|-------|------|-------------------------------|-----------------------------|----------------------------------------|
| Age (years) | 30.8 (29 – 33) | n/a | n/a | n/a |
| coronal ratio tibial footprint | 0.506 (0.501 – 0.512) | 0.827 with CI 95% (-0.204 – 0.981) | 0.831 with CI 95% (-0.133 – 0.983) | 0.891 with CI 95% 0.589 – 0.987 |
| sagittal ratio tibial footprint | 0.429 (0.405 – 0.441) | 0.816 with CI 95% (-0.213 – 0.980) | 0.994 with CI 95% (0.953 – 0.999) | 0.953 with CI 95% (0.787 – 0.995) |
| sagittal ratio femoral foot‑print high to low | 0.222 (0.203 – 0.237) | 0.922 with CI 95% (0.180 – 0.992) | 0.889 with CI 95% (-0.120 – 0.989) | 0.940 with CI 95% (0.662 – 0.993) |
| sagittal ratio femoral foot‑print deep to shallow | 0.370 (0.36 – 0.38) | 0.977 with CI 95% (0.770 – 0.998) | 0.985 with CI 95% (0.880 – 0.999) | 0.968 with CI 95% (0.850 – 0.996) |
| α | 34.243° (31.488 – 35.393) | 0.934 with CI 95% (0.005 – 0.994) | 0.991 with CI 95% (0.935 – 0.999) | 0.962 with CI 95% (0.841 – 0.996) |
| β | 86.967° (86.129 – 87.579) | 0.922 with CI 95% (0.234 – 0.992) | 0.783 with CI 95% (-0.085 – 0.977) | 0.879 with CI 95% (0.544 – 0.986) |
| coronal articular surface and ACL—angle | 73.309° (72.635 – 74.048) | 0.943 with CI 95% (0.586 – 0.994) | 0.936 with CI 95% (0.470 – 0.993) | 0.967 with CI 95% (0.873 – 0.996) |
| sagittal articular surface and ACL—angle | 60.253° (59.980 – 60.550) | 0.980 with CI 95% (0.827 – 0.998) | 0.963 with CI 95% (0.665 – 0.996) | 0.986 with CI 95% (0.944 – 0.998) |
| sagittal articular surface and Blumensaat’s line—angle | 58.634° (57.691 – 58.989) | 0.990 with CI 95% (0.889 – 0.999) | 0.989 with CI 95% (0.855 – 0.999) | 0.975 with CI 95% (0.902 – 0.997) |

identification of anatomical femoral and tibial ACL’s footprints.

Disclosures
Each author certifies that his institution has approved the reporting of this case series that all investigations were conducted in accordance with the Declaration of Helsinki and Guidelines for Good Clinical Practice.

Abbreviations
ACL: Anterior cruciate ligament; AP: Anteroposterior; CI: Confidence intervals; CLASS: Compressed Lateral and anteroposterior Anatomical Systematic Sequences; DS: Deep to shallow; HL: High to low; ICC: Intraclass correlation coefficient; LAT: Lateral; α: Femoral intercondylar notch roof angle; β: Proximal tibial slope.

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Authors’ contributions
Grégoire Thürig contributed substantially to the design, analysis, interpretation of data and drafting of the work. Raoul Panadero-Morales contributed substantially to the design and revising the work critically for important intellectual content. Luca Giovannelli contributed substantially to the design and revising the work critically for important intellectual content. Franziska Kocher contributed substantially to the analysis and revising the work critically for important intellectual content. José Louis Peris contributed substantially to the design and revising the work critically for important intellectual content. Kocher contributed substantially to the design and revising the work critically for important intellectual content. Montiz Tannast contributed substantially to revising the work critically for important intellectual content and final approval. All authors read and approved the final manuscript.

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Declarations
Ethics approval and consent to participate
The study was carried out following the World Medical Association Declaration of Helsinki. According to federal law, our project did not need the approval of the local ethical committee (http://www.cervvd.ch/ soumission/premiers‑pas.html).

Competing interests
There is no conflict of interest.

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References
1. Amis AA, Jakob RP (1998) Anterior cruciate ligament graft positioning, tensioning and twisting. Knee Surgery, Sport Traumatol Arthrosc 6:2–12
2. Amis AA, Zavras TD (1995) Isometricity and graft placement during anterior cruciate ligament reconstruction. Knee 2:5–17
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tibial slope.
anterior cruciate ligament insertion site anatomy. Knee Surgery, Sport Traumatol Arthrosc: Springer, Berlin Heidelberg 26:1311–1318.

4. Bedi A, Maak T, Musahl V, Citak M, O’Loughlin PF, Choi D, Pearle AD (2011) Effect of tibial tunnel position on stability of the knee after anterior cruciate ligament reconstruction. Is the tibial tunnel position most important? Am J Sports Med 39:366–373.

5. Bernard M, Hertel P, Hornung H, Cierpinski T (1997) Femoral insertion of the ACL: Radiographic quadrant method. Am J Knee Surg 10:14–21 (discussion 21 2).

6. Byrne KJ, Hughes JD, Gibbs C, Vaswani R, Meredith SJ, Popchak A, Lesniak BP, Karlsson J, Irrgang JJ, Musahl V (2021) Higher frequency of osteoarthritis in patients with ACL graft rupture than in those with intact ACL grafts 30 years after reconstruction. Knee Surgery, Sport Traumatol Arthrosc: Springer, Berlin Heidelberg 28:2139–2146.

7. Carbone A, Rodeo S (2017) Review of current understanding of post-traumatic osteoarthritis resulting from sports injuries. J Orthop Res 35:397–405.

8. Cheung EC, DiLallo M, Feeley BT, Lansdown DA (2020) Osteoarthritis and ACL Reconstruction—Myths and Risks. Curr Rev Musculoskelet Med Current Reviews in Musculoskeletal Medicine 13:115–122.

9. Cho HJ, Kim TK, Kang SB, Do MU, Chang CB (2017) Variations in sagittal locations of anterior cruciate ligament tibial footprints and their association with radiographic landmarks: a human cadaveric study. BMC Musculoskeletal Disorders 18:1–8.

10. Gomoll AH, Bach BR (2006) Managing Tunnel Malposition and Widening of the ACL. Oper Tech Sports Med 14:36–44.

11. Hart A, Sivakumaran T, Burman M, Powell T, Martineau PA (2018) A Prospective Evaluation of Femoral Tunnel Placement for Anatomic Anterior Cruciate Ligament Reconstruction Using 3-Dimensional Magnetic Resonance Imaging. Am J Sports Med 46:192–199.

12. Hwang MD, Piefer JW, Lubowitz JH (2012) Anterior Cruciate Ligament Tibial Footprint Anatomy: Systematic Review of the 21st Century Literature. Arthroscopy Elsevier Inc 28(S):728–734.

13. Iriuchishima T, Goto B (2021) Systematic Review of Surgical Technique and Tunnel Target Points and Placement in Anatomical Single-Bundle ACL Reconstruction. J Knee Surg 34:1531–1538.

14. Kumar S, Kumar A, Kumar R (2017) Accurate Positioning of Femoral and Tibial Tunnels in Single Bundle Anterior Cruciate Ligament Reconstruction Using the Indigenously Made Bernard and Hurtle Grid on a Transparency Sheet and C-arm. Arthrosc Tech Arthroscopy Association of North America 6:e757–e761.

15. Lippis DB, Wilson AM, Ashton-Miller, JA, Wojtys EM (2012) Evaluation of different methods for measuring lateral tibial slope using magnetic resonance imaging. Am J Sports Med 40:2731–2736.

16. Majewski M, Susanne H, Klaus S (2006) Epidemiology of athletic knee injuries: A 10-year study. Knee 13:184–188.

17. Montgomery AA, Grahams A, Evans PH, Fahey T (2002) Interrater agreement in the scoring of abstracts submitted to a primary care research conference. BMC Health Serv Res 2:1–4.

18. Parkar AP, Adraeensens MEAPM, Vindfeld S, Solheim E (2017) The Anatomic Centers of the Femoral and Tibial Insertions of the Anterior Cruciate Ligament: A Systematic Review of Imaging and Cadaveric Studies Reporting Normal Center Locations. Am J Sports Med 45:2180–2188.

19. Piefer JW, Pflugner TR, Hwang MD, Lubowitz JH (2012) Anterior Cruciate Ligament Femoral Footprint Anatomy: Systematic Review of the 21st Century Literature. Arthroscopy Elsevier Inc 28(s):872–881.

20. Robinson J, Inderhaug E, Harlem T, Spalding T, Brown CH (2020) Anterior Cruciate Ligament Femoral Tunnel Placement: An Analysis of the Intended Versus Achieved Position for 221 International High-Volume ACL Surgeons. Am J Sports Med 48:1088–1099.

21. Scanlan SF, Lai J, Donahue JP, Andriacchi TP (2012) Variations in the three-dimensional location and orientation of the ACL in healthy subjects relative to patients after transtibial ACL reconstruction. J Orthop Res 30:910–918.

22. Scheffler SU, Maschewski K, Becker R, Asbach P (2018) In-vivo three-dimensional MRI imaging of the intact anterior cruciate ligament shows a variable insertion pattern of the femoral and tibial footprints. Knee Surgery, Sport Traumatol Arthrosc: Springer, Berlin Heidelberg 26:3667–3672.

23. Schneider CA, Rasband WS, Eliceiri KW (2012) NIH Image to ImageJ: 25 years of image analysis. Nat Methods Nature Publishing Group 9:671–675.

24. Sivakumaran T, Jaffer R, Marwan Y, Hart A, Radu A, Burman M, Martineau PA, Powell T (2021) Reliability of Anatomic Bony Landmark Localization of the ACL Femoral Footprint Using 3D MRI. Orthop J Sport Med 9:1–6.

25. Söderman T, Wettling ML, Hänni M, Mikkelsen C, Johnson RJ, Werner S, Sundin A, Shalabi A (2020) Higher frequency of osteoarthritis in patients with ACL graft rupture than in those with intact ACL grafts 30 years after reconstruction. Knee Surgery, Sport Traumatol Arthrosc: Springer, Berlin Heidelberg 28:2139–2146.

26. Zavras TD, Race A, Amis AA (2005) The effect of femoral attachment location on anterior cruciate ligament reconstruction: Gift tension patterns and restoration of normal anterior-posterior laxity patterns. Knee Surgery, Sport Traumatol Arthrosc: 13:92–100.

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