Exploring New Strategies to Monitor Autophagy and Related Cell Death Pathways Using Raman Spectroscopy

Martin Isabelle1,2, Vincent I Poon2, Zoe V Petropoulos3, Samantha J Harder1, Julian J Lum2,3

1Department of Physics and Astronomy, University of Victoria, 3800 Finnerty Rd, Victoria, BC V8P 5C2, Canada
2Trev and Joyce Deeley Research Centre, British Columbia Cancer Agency, 2410 Lee Avenue, Victoria, BC, V8R 6V5, Canada
3Department of Biochemistry and Microbiology, University of Victoria, 3800 Finnerty Rd, Victoria, BC V8P 5C2, Canada

*Corresponding author: Julian J Lum, Trevand Joyce Deeley Research Centre, British Columbia Cancer Agency, 2410 Lee Avenue, Victoria, BC, V8R 6V5, Canada; E-mail: JLum@bccancer.bc.ca

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Autophagy in the context of cancer

Macrouautophagy, (hereafter referred to as autophagy) is thought to play a pivotal role in tumorigenesis and tumor cell survival. Autophagy is a self-degradative cellular process that recycles intracellular components such as proteins and lipids, and may also be used to clear extraneous or damaged organelles. Through this process, metabolites such as amino acids or fatty acids can be liberated for use by the cell. While basal levels of autophagy are required for cellular homeostasis, autophagy is most commonly induced in response to metabolic stressors. In this way, autophagy may be utilized by cancer cells to adapt to the tumor microenvironment, which may be hypoxic and/or nutrient low, or as an adaptive response to cytotoxic insult by chemotherapeutic agents. Conversely, excessive or dysregulated autophagy may be part of the cell death pathway continuum, having been previously implicated in both apoptosis and necrosis [1,2]. In addition, down regulation of tumor autophagy may promote immune evasion by disrupting the antigen-processing pathway [3,4]. Therefore, further investigation of autophagy’s role in tumor cell survival and death is warranted.

Mechanism of action in autophagy

At each step of autophagy, a highly ordered and defined biochemical reorganization is executed, and these changes may be used as markers to detect autophagy. The mammalian Target of Rapamycin (mTOR) has a central role in the nutrient-sensing pathway, and serves to inhibit autophagy via phosphorylation of the autophagy-initiating ULK1/2 complex in times of plenty [5]. Stressors such as hypoxia, nutrient depletion or DNA damage lead to inhibition of mTOR activity, as well as activity of the autophagy-activating Beclin1 protein, resulting in a large shift in cellular programming [6]. However, autophagy regulation is complex, and involves a number of cellular pathways including the modulation of transcription factors and post-translational protein modification [7]. Regardless, upon initiation of autophagy, the microtubule-associated protein 1A/1B-light chain 3 (LC3) undergoes a cleavage event, denoted as a shift from LC3-I to LC3-II [8]. LC3-II then associates with phosphatidylethanolamine bound to both sides of the membrane, which promotes asymmetric membrane curvature, and after further elongation of the membrane, helps form the autophagic vesicle (the autophagosome). During formation, the autophagosome may non-selectively engulf cytosolic components, or selectively traffic contents to be degraded, such as lipid droplets, damaged organelles or misfolded proteins [9-12]. Finally, the autophagosome eventually fuses with a lysosome in a pH-dependent manner, after which acid hydrolases breakdown the vesicle components, releasing metabolites back into the cytosol.

Current methods and challenges in autophagy detection

Autophagy has been assessed using electron microscopy, fluorescence microscopy and immunoblotting of autophagy-related proteins [13-17]. In vitro, the most common approach to measure autophagy induction is using the autophagic flux assay, where changes in the cleavage patterns of LC3 are monitored. Generally, LC3-II is measured via immunoblotting of autophagy re-
niques to measure the turnover of cytosolic proteins, or the activity of transcriptional regulators, such as mTOR. *Ex vivo*, the current gold standard for characterizing autophagy is the use of transmission electron microscopy to identify autophag-ic vesicles. Formalin-fixed paraffin-embedded tissue sections may also be used to probe for changes in autophagy-related proteins such as Beclin1 or LC3a [18]. However, the resolution of immunohistochemical staining is currently limited, and due to other biological roles of Beclin and LC3, the data collected thus far using these assays is correlative.

All of these techniques are invasive and require some modification of the cells either using a fluorescent reporter construct (e.g. GFP-LC3 constructs), fixation, staining or samples being placed in a vacuum. They are also expensive, time-consuming, and require operation of equipment by highly skilled personnel. There is a significant need, especially for primary human tissues, for a highly specific and sensitive marker for autophagy. In this commentary, we provide a rationale to explore using Raman Spectroscopy (RS) for this purpose.

**Applications of Raman Spectroscopy in cellular systems**

Spectroscopy, the study of the interaction of electromagnetic radiation with matter, is an important biochemical tool that can be used to probe the structure and composition of molecules in a biological sample. There are many different types of spectroscopy used in biochemistry which include: emission spectroscopy (i.e. fluorescence and phosphorescence), absorption spectroscopy (e.g. infrared and ultraviolet-visible), elastic scattering and reflection spectroscopy, resonance spectroscopy (e.g. nuclear magnetic resonance), and inelastic scattering spectroscopy (i.e. Raman and Compton scattering). The most common types of spectroscopy used in biochemistry are fluorescence, infrared, visible, Ultraviolet (UV), and nuclear magnetic resonance spectroscopy. RS is a vibrational spectroscopic method in which monochromatic light incident on a sample is inelastically scattered, collected and dispersed via a grating spectrometer onto a detector. The energy required to excite a molecular vibration depends on the masses of the atoms involved in the vibration and the type of chemical bonds between these atoms. It also may be influenced by the structure, interactions and the chemical microenvironment of the molecule.

These vibrational signatures provide a “molecular fingerprint” of components within the biological sample related to proteins (e.g amino acids, conformational structures), nucleic acids (DNA and RNA), carbohydrates (e.g. glucose and glycogen) and lipids (e.g. cholesterol, choline, CH2 groups). It is the positions, relative intensities and shapes of these bands in a Raman spectrum that carry detailed information about the molecular composition of the sample. Advanced chemometric statistical analytical tools can be used to extract relevant biochemical information from large data sets or identify complex spectral trends.

RS has proven useful in a range of biological and medical applications. Particularly, RS has been utilized in oncology by offering an objective technique for diagnosis and monitoring of cellular processes. It has been used in the study and diagnostics of several types of cancer including skin [19], bladder [20], breast [21,22], and cervical [23]. Analysis of tissue samples, single cells and biological fluids is possible due to its versatile nature, and RS has been used for biochemical analysis of various cell processes including cell proliferation [24], differentiation [25], autophagy [26] and cell death [17]. Currently the most conventional form of RS used in medical research is dispersive and confocal Raman microspectroscopy for *ex vivo* applications. However, in the last decade, there have been a number of studies using Raman spectroscopy probes that do not require the removal of tissue or cells for analysis but instead, can be used as an *in vivo* diagnostic tool [27-29]. As well as those mentioned above, RS has additional advantages over current biomedical technologies that analyze biological cells and tissue. RS can be used in aqueous solutions, measurements need only a relatively short amount of time to be performed (10 to 30 seconds) and RS has higher resolving powers compared to its spectroscopic counterparts (e.g. 1µm spatial resolution in the most optimal system) which allows for intracellular and even subnuclear structural imaging and analysis of cells [30].

The main difficulties of Raman spectroscopy have come from its weak scattering signal compared to its counterpart, Rayleigh elastic scattering, which is 107 times stronger in signal. In order to resolve this issue, modern Raman spectroscopic systems have incorporated technology such as multiple monochromators and Rayleigh holographic notch filters in order to reducing the elastic Rayleigh scattering, and improve signal to noise.

**Raman Spectroscopy in autophagy**

Konorov et al. [26] assessed RS in autophagy using metastatic prostate carcinoma cells and human breast carcinoma cells exposed to starvation conditions (glutamine deprivation and amino acid deprivation). Prior to RS cell measurements, fluorescence microscopy was used to assess the response of the cells to starvation conditions using the GFP-LC3 reporter construct. Increased numbers of GFP-LC3-positive puncta were clearly visible after one day of glutamine deprivation indicative of autophagosome formation during autophagy. In the MCF7 human breast carcinoma cells, the average autophagosome content per cell increased 2.9 times (from 9.1 to 26.4) in the absence of glutamine while metastatic prostate carcinoma cells increased 2.1 times (from 5.5 to 11.6). RS of the cells during starvation conditions revealed increases in the phospholipid 718 cm⁻¹ Raman band, indicating accumulation of double-membrane autophagic vesicles. There was also a decrease in the 937 cm⁻¹ and 1003 cm⁻¹ Raman bands potentially attributed to degradation of proteins due to autophagy, which is indicative of an autophagic response to starvation stimuli. The authors concluded that the intensity of the 718 cm⁻¹ Raman band relative to the 784 cm⁻¹ (DNA-associated, accounting for variation in cell cycle phase in cells) intensity could be a useful spectral marker for monitoring cellular response to starvation stimuli. As illustrated in Figure 1, various examples of biomolecular signatures may be assessed by Raman spectroscopy to indicate the different stages of autophagy. For example, formation of double membrane vesicles results in increases in phospholipid
bands at 718 cm⁻¹, while degradation of complex biomolecules (e.g., proteins and lipids) into their constituent monomer units (amino acids, fatty acids, and glycerol) are visualized by changes in peak intensities (1657-1660 cm⁻¹ and 1448 cm⁻¹).

### Raman Spectroscopy in apoptosis and necrosis

Raman spectroscopy has also been used to study and discriminate apoptosis and necrosis in cancer cells. Apoptosis is the process of programmed cell death that involves a series of biochemical events leading to morphological changes including blebbing, loss of membrane attachment, cell shrinkage, nuclear fragmentation, chromatin condensation, chromosomal DNA fragmentation, and formation of apoptotic bodies. Apoptosis is usually beneficial to the organism, taking place during embryonic development or preventing tumor formation by acting as a homeostatic regulator of cell death and mitotic rates. Necrosis, in contrast, is the premature death of cells and tissue caused by factors external to cells (e.g., infection, toxin or trauma). Events such as organelle membrane disruption and hypoxia are triggers of necrosis, resulting in ATP depletion, metabolic collapse, cell swelling, and rupture, leading to inflammation. Discrimination between apoptotic and necrotic cell death is technically challenging in vitro, and relies heavily upon pathologist experience in ex vivo settings.

**Kunapareddy et al. [16]** used RS to characterize necrotic cell death. Necrosis in human malignant melanoma cell line (MEL-28) was induced through a combination of oxygen and glucose deprivation. RS of nonproliferating live cells and dead cells were taken and basis spectra of protein, lipid, RNA, DNA, and glycogen were fitted to each of the cell spectra. Decreases in the relative amounts of lipid (717, 935, 1085, 1448, 2854 and 2896 cm⁻¹) and RNA (900, 1092, and 1575 cm⁻¹), and an increase in the relative protein content (642, 827, 1395 to 1425 cm⁻¹) were observed in dead cells. As the authors indicated, this is consistent with the process of coagulative necrosis which features destruction of cytoplasmic structures and degradation of the membranes in the first stages of necrosis. They also observed Raman band changes in protein amide I bands (from 1657 cm⁻¹ in live cells to 1660 cm⁻¹ in dead cells) indicating conformational and composition changes in protein and nucleic acid in dead cells.

In vitro, apoptosis may be detected through Annexin V staining, which binds to phosphatidylserine exposed during early stages of apoptosis, caspase activation, or DNA fragmentation assays; unfortunately, many of these markers are also seen in necrotic cells. From tissue sections, caspase cleavage and cellular morphology are commonly used to distinguish apoptosis and necrosis, and these remain qualitative measures. Thus, new techniques to distinguish these modes of cell death are needed.

Figure 1 - Characteristics of Autophagy measurable via Raman Spectroscopy
Apopotic cell death was studied in RS by Verrier et al. [17] who used Raman microspectroscopy to assess molecular changes in human lung carcinoma epithelial cells (A549) induced into apoptotic cell death using Triton X-100. They observed decreases in DNA (788 cm⁻¹) by 80% after 72 hours of treatment indicating phosphodiester bonds breakage as a result of fragmentation and disintegration of the DNA strands which was confirmed by DNA integrity assays. The authors also observed a 45% decrease in protein (632, 645, 854, 938, 1005 and 1342 cm⁻¹) explained by protein cleavage following caspase activation. An increase in lipid concentration was also found (1660 and 1743 cm⁻¹). These lipid changes were also observed in Etoposide-treated (apoptotic) human breast cancer cells from another study by Zoladek [15] et al. Etoposide-treated cancer cells showed a high accumulation of both membrane and non-membrane lipids (triglycerides) correlating to formation of large numbers of lipid vesicles in apoptotic cells. The increase in triglyceride non-membrane bound lipids in apoptotic cells was thought to be due to the inhibition of phosphatidicholine biosynthesis, activation of phospholipases, and the formation of lipid bodies already seen in cells exposed to acidic pH [31,32], cells engaged in inflammation [33] or apoptotic cells [34]. However contrary to findings by Verrier et al.[17] Raman bands assigned to DNA also increased in apoptotic cells, which was attributed to nuclear condensation.

RS, in combination with machine learning chemometrics, has also been used to discriminate between apoptosis and necrotic cell death [35]. A549 lung epithelia cells were forced into necrosis (using Triton X-100) or apoptosis (using etoposide). Raman spectra were collected from both cell death states, and support vector machines (SVMs) machine learning was applied to test the ability of RS to classify correct states of cell death. SVM classifiers were successfully able to discriminate the control cells from cells treated with etoposide or Triton X-100.

Summary

These Raman studies demonstrate the uniqueness of Raman spectroscopy to be able to obtain vast biochemical information (particularly lipid, protein and DNA relative intensity changes) from live and dead cancer cells non-invasively (as illustrated in Figure 1), without the use of fluorescent reporter constructs, labels, stains or contrasting-enhancing techniques. Differentiation of autophagy, apoptosis and necrotic cell death is important in biomedical sciences, especially in cancer treatment. Autophagy may suppress the initiation of cancer growth, promote cancer cell survival, or play a role in cell death. Therefore improved detection, discrimination and understanding of autophagy and related cell death processes will enable improved and optimized treatment plans for cancer therapy through assessing cellular response to chemotherapy, radiotherapy and other cancer-targeted treatments and differentiating between autophagy, apoptosis and necrosis occurring in cells.

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