Tractable Dendritic RNNs for Reconstructing Nonlinear Dynamical Systems

Manuel Brenner * 1 2 Florian Hess * 1 2 Jonas M. Mikhaeil 1 2 Leonard Bereska 1 3 Zahra Monfared 1 Po-Chen Kuo 4 Daniel Durstewitz 1 2

Abstract

In many scientific disciplines, we are interested in inferring the nonlinear dynamical system underlying a set of observed time series, a challenging task in the face of chaotic behavior and noise. Previous deep learning approaches toward this goal often suffered from a lack of interpretability and tractability. In particular, the high-dimensional latent spaces often required for a faithful embedding, even when the underlying dynamics lives on a lower-dimensional manifold, can hamper theoretical analysis. Motivated by the emerging principles of dendritic computation, we augment a dynamically interpretable and mathematically tractable piecewise-linear (PL) recurrent neural network (RNN) by a linear spline basis expansion. We show that this approach retains all the theoretically appealing properties of the simple PLRNN, yet boosts its capacity for approximating arbitrary nonlinear dynamical systems in comparatively low dimensions. We employ two frameworks for training the system, one combining back-propagation-through-time (BPTT) with teacher forcing, and another based on fast and scalable variational inference. We show that the dendritically expanded PLRNN achieves better reconstructions with fewer parameters and dimensions on various dynamical systems benchmarks and compares favorably to other methods, while retaining a tractable and interpretable structure.

1. Introduction

For many complex systems in physics, biology, or the social sciences, we do not know or have only rudimentary knowledge about the dynamical system (DS) that may underlie those quantities that we can empirically observe or measure. Data-driven approaches aimed at automatically inferring the generating DS from time-series observations could therefore strongly support the scientific process, and various such methods have been proposed in recent years (Raissi et al., 2018; Zhu et al., 2021; Yin et al., 2021; Norcliffe et al., 2021; Mohajerin & Waslander, 2018; Karl et al., 2017; Chen et al., 2018; Strauss, 2020). However, due to the often high-dimensional, complex, chaotic, and inherently noisy nature of real-world DS, like the brain, weather-, or ecosystems, this remains a formidable challenge. Moreover, although the true DS may evolve on a lower-dimensional manifold in its state space, the system used for approximating usually needs to be of higher dimensionality to achieve a proper embedding (Takens, 1981; Sauer et al., 1991; Kantz & Schreiber, 2004). This is especially true when the approximating system is of a different functional form than the one that would most naturally describe the data generation process (but is unknown), for instance, when we attempt to approximate a system of exponential or trigonometric functions by polynomials.

In this work we sought to improve the capacity and expressiveness of a specific class of recurrent neural networks (RNNs), achieving agreeable solutions with fewer dimensions and parameters while retaining a set of desirable theoretical properties. Specifically, we build on piecewise-linear RNNs (PLRNNs) based on ReLU activation functions, for which fixed points, periodic orbits, and other dynamical properties can be derived analytically (Schmidt et al., 2021; Koppe et al., 2019), and for which dynamically equivalent continuous-time (ordinary differential equation, ODE) systems can be constructed (Monfared & Durstewitz, 2020b). Inspired by principles of dendritic computation in biological neurons (Fig. 1), each PLRNN unit was endowed with a set of nonlinear pre-processing subunits (“dendritic branches”), such that it effectively takes on the role of an equivalent much larger network. Mathematically, this comes down, in our case, to enhancing each latent unit with a linear spline basis expansion as popular in statistics (Hastie et al.,...
works aimed at directly learning the system’s underlying DS (LASSO) (Brunton et al., 2016; Rudy et al., 2017; de Silva et al., 2020) or when the underlying systems are very high-dimensional, comparatively short trajectories were empirically observed (Kanter & Schreiber, 2004; Bakarji et al., 2018). Importantly, we prove that these modifications preserve the mathematical and dynamical accessibility of the resulting system, e.g., such that fixed points, cycles, and their stability, can still be computed analytically.

Besides its effectiveness in capturing complex dynamical systems in fewer dimensions within a tractable framework, our approach highlights more generally how principles of dendritic signal processing may be harvested in the design of RNNs. Strongly nonlinear local computations are known for decades to occur within dendritic trees of biological neurons (Mel, 1994; Poirazi et al., 2003), but have hardly been exploited so far for machine learning models.

2. Related Work

One class of DS reconstruction models attempts to discover governing equations from the vector field estimated from data through differencing the time series. Sparse Identification of Nonlinear Dynamics (SINDy), for instance, does so by sparsely regressing on a rich library of basis functions using the least absolute shrinkage and selection operator (LASSO) (Brunton et al., 2016; Rudy et al., 2017; de Silva et al., 2020). Other methods approximate the vector field using additive ODE models (Chen et al., 2017), sparse auto-encoders (Heim et al., 2019), shallow ‘multi-layer’ perceptrons reformulated as RNNs (Trischler & D’Eleuterio, 2016), or deep neural networks (Chen et al., 2018). Some works aimed at directly learning the system’s underlying Hamiltonian (Chen et al., 2020; Greydanus et al., 2019).

Generally, numerical derivatives obtained from time series tend to be more noise-prone than the time series observations themselves (Baydin et al., 2018; Chen et al., 2017; Raissi, 2018). This can be a problem particularly if only comparatively short trajectories were empirically observed or when the underlying systems are very high-dimensional, as in these cases the system’s vector field may be (severely) under-sampled. Methods directly based on numerical derivatives also need to be augmented by other techniques, like delay embeddings (Kantz & Schreiber, 2004; Bakarji et al., 2022), if not all the system’s dimensions were observed.

Various RNN architectures such as Long-Short-Term-Memory networks (LSTMs) (Zheng et al., 2017), Reservoir Computing (RC) (Pathak et al., 2018), or PLRNNs (Koppe et al., 2019; Schmidt et al., 2021) have been employed to infer DS directly from the observed time series without going through numerical derivatives. More generally, a wide array of RNN architectures with specific functional or parametric forms, e.g. based on coupled oscillators (Rusch & Mishra, 2021), has been proposed in recent years (Kerg et al., 2019; Chang et al., 2019; Erichson et al., 2021; Kag et al., 2020; Rusc et al., 2022), mainly in order to tackle the exploding/vanishing gradient problem in RNN training (Bengio et al., 1994; Hochreiter & Schmidhuber, 1997). In the present context it is important to note, however, that most of these are not suitable for DS reconstruction since their functional form or specific parameterization strictly delimits the range of DS phenomena they can learn or generate. For instance, chaotic dynamics are not possible in any of these latter systems by mathematical design (Monfared et al., 2021), with the only exception of Long-Expressive-Memory (LEM) networks (Rusch et al., 2022). More recently, transformers (Shalova & Oseledets, 2020a;b) were used as black box approaches for DS prediction.

Except for PLRNNs, however, all of the approaches reviewed above, even those specifically designed for DS reconstruction and prediction, rest on relatively complex model formulations that are not easy to tackle and analyze from a DS perspective (Fraccaro et al., 2016). The ability to gain deeper insights into the specific DS properties and mechanisms of the recovered system is, however, often crucial for its applicability to science and engineering problems. Transformers, unlike RNNs, do not even constitute DS themselves (as they explicitly forgo any temporal recursions), and therefore are not directly amenable to DS theory tools. Moreover, most of these models, RC in particular, need very high-dimensional latent spaces, which further adds to their black-box nature.

Better interpretability and tractability is achieved by using PLRNNs (Koppe et al., 2019; Schmidt et al., 2021) or by (locally) linearizing nonlinear systems through ideas from Koopman operator theory (Azenet et al., 2020; Brunton et al., 2017; Yeung et al., 2017). In such systems, certain DS properties can be analytically accessed (Schmidt et al., 2021; Monfared & Durstewitz, 2020a). On the downside, usually one needs to move to very high dimensions to represent the DS in question properly. Here we aim to overcome this limitation by augmenting PLRNNs with linear basis expansions without altering their analytical accessibility.

Finally, probabilistic (generative) latent variable models such as state space models have been applied to the problem of posterior inference of latent state paths \( x_t \sim p(x_t | z_{1:T}) \) of DS given time series observations \( z_{1:T} \) (Pandarinath et al., 2018; Ghahramani & Roweis, 1998; Durstewitz, 2017; Krishnan et al., 2017). The advantage here is that they also account for uncertainty in the model formulation or latent
process itself and yield the full distribution over latent space variables (Karl et al., 2017). For DS reconstruction, however, we need to move beyond posterior inference: We require that samples drawn from the model’s prior distribution \( p(z) \) after training exhibit the same (invariant) temporal and geometric structure as those produced by the unknown DS, a property that is not automatically guaranteed in this class of algorithms.

Here we show that PLRNNs augmented with a linear spline expansion can be most efficiently trained by BPTT using a specific form of TF (Appx. 6.1). We also embed expanded PLRNNs into a fully probabilistic, variational approach that scales well with system size by employing stochastic gradient variational Bayes (SVGB; (Kingma & Welling, 2014; Rezende et al., 2014)), thereby combining the advantages of the two classes of models reviewed above, but with mild detriments in DS reconstruction performance compared to BPTT.

3. Model Formulation and Theoretical Considerations

3.1. Piecewise Linear Recurrent Neural Network (PLRNN)

Our approach builds on PLRNNs (Durstewitz, 2017; Koppe et al., 2019) because of their mathematical tractability (see Sec. 3.3). PLRNNs are defined by the \( M \)-dimensional latent process equation

\[
z_t = A z_{t-1} + W \phi(z_{t-1}) + h + C s_t,
\]

which describes the temporal evolution of \( M \)-dimensional latent state vector \( z_t = (z_{1t}, \ldots, z_{Mt})^T \). The self-connections of the units are represented by diagonal matrix \( A \in \mathbb{R}^{M \times M} \), whereas the connections between units are collected in off-diagonal matrix \( W \in \mathbb{R}^{M \times M} \), with the nonlinear activation function \( \phi \) given by the rectified linear unit (ReLU) applied element-wise:

\[
\phi(z_{t-1}) = \max(0, z_{t-1}).
\]

The diagonal terms in \( A \) can be interpreted as the system’s “passive” (in the absence of inputs) time constants such that different latent states may capture different time scales of the underlying DS (as illustrated in Fig. S1; see also Schmidt et al. (2021)). The PLRNN also has a bias term \( h \in \mathbb{R}^M \) and accommodates potential external inputs \( s_t \in \mathbb{R}^K \) weighted by \( C \in \mathbb{R}^{M \times K} \). In a fully probabilistic framework, furthermore a Gaussian noise term \( \epsilon_t \sim \mathcal{N}(0, \Sigma) \) with diagonal covariance \( \Sigma \) is added to Eq. 1. The PLRNN can be interpreted as a discrete-time neural rate model (Durstewitz, 2017), where the entries of \( A \) stand for the individual neurons’ time constants, \( W \) for the synaptic connection strengths between neurons, and \( \phi(z) \) for a (ReLU-shaped) voltage-to-spike-rate transfer function. The latent RNN Eq. 1 is linked to the \( N \)-dimensional observed time series \( (x_t)_{t=1}^T, x_t \in \mathbb{R}^N \), drawn from an underlying noisy DS, by an observation function (decoder model) which, in the simplest case, may take the linear Gaussian form

\[
x_t = B z_t + \eta_t,
\]

where \( B \in \mathbb{R}^{N \times M} \) represents a factor loading matrix and \( \eta_t \sim \mathcal{N}(0, \Gamma) \) is Gaussian observation noise with diagonal covariance \( \Gamma \in \mathbb{R}^{N \times N} \) (only explicitly estimated as a free parameter in the variational approach).

3.2. Dendritic Computation and Spline Basis Expansion

Dendrites have long been known to play an active and important part in neural computation (Mel, 1994; 1999; Koch, 2004). Active, fast voltage-gated ion channels endow dendrites with strongly nonlinear behavior, giving rise for instance to dendritic Ca\(^{2+}\) spikes that boost synaptic inputs (Schiller et al., 2000; Häusser et al., 2000). It has been suggested previously that different dendritic branches may constitute rather independent computational sub-units whose outputs are combined at the soma, as in a 2-layer neural network (Poirazi et al., 2003; Mel, 1993; 1994), an idea that received strong empirical support especially in recent years (Poirazi & Papoutsi, 2020). Here we mimic this functional setup by modeling dendritic processing through a linear combination of ReLU-type threshold-nonlinearities (Fig. 1), replacing Eq. 2 by

\[
\phi(z_{t-1}) = \sum_{b=1}^B \alpha_b \max(0, z_{t-1} - h_b),
\]

with “dendritic input/output” slopes \( \alpha_b \in \mathbb{R} \) and “activation” thresholds \( h_b \in \mathbb{R}^M \). As in real dendrites, where both ion channels and morphological structure are subject to learning (Poirazi & Papoutsi, 2020; Stemmler & Koch, 1999), we treat these as trainable parameters. To emphasize the connection to dendritic computation we call the system Eqs. 1, 3, 4, the *dendPLRNN*.

We note that Eq. 4 inserted into model Eq. 1 takes the form of a linear spline basis expansion as popular in statistics and machine learning (Hastie et al., 2009) for approximating arbitrary functions (Wahba, 1990; Storace & De Feo, 2004) in regression settings and other model-based approaches. In our context of DS reconstruction, however, there are particular challenges associated with such an approach, as we would like to preserve certain mathematical properties of the expanded model for its DS tractability. This is indeed one major contribution of the present work and addressed in the next section.
### 3.3. Mathematical Tractability and Dynamical Systems

**Interpretation**

Sharp threshold-nonlinearities (like a ReLU) are a reasonable choice from a neurobiological perspective, as dendrites naturally give rise to this threshold-type behavior (Mel, 1999; Koch, 2004). Another important consideration in choosing this particular form, however, was that it preserves all the theoretically appealing properties of a PLRNN, as we will formally establish below: For PLRNNs fixed points and cycles can be explicitly computed (Schmidt et al., 2021; Koppe et al., 2019), and they can be translated into dynamically equivalent continuous-time systems (Monfared & Durstewitz, 2020b), properties which profoundly ease the analysis of trained systems from a DS perspective.1 This is crucial for application in the sciences, where we are specifically interested in understanding the underlying system’s dynamics. For PLRNNs, precise connections between the long-term behavior of the system and that of its gradients have also been established (Schmidt et al., 2021; Monfared et al., 2021). Finally, PLRNNs belong to the class of continuous piecewise-linear (PWL) maps, for which many important types of bifurcations have been well characterized (Feigin, 1995; Hogan et al., 2007; Patra, 2018) (see Monfared & Durstewitz, 2020a) for an overview). Bifurcations are essential to understand how geometrical and topological properties of the system’s state space depend on its parameters or could be controlled, and hence are also important to characterize or improve the training process itself (Doya, 1992; Pascuau et al., 2013; Saxe et al., 2014), or to understand properties of trained systems (Maheswaranathan et al., 2019a; b).

Our first proposition, therefore, assures that by the particular form of basis expansion introduced in Eq. 4, the system will remain within the class of continuous PWL maps:

**Proposition 1.** The model defined through Eq. 1 and Eq. 4 constitutes a continuous PWL map.

The proof essentially straightforwardly follows from the model’s definition as a linear spline basis expansion in each unit, but is formally provided in Appx. 6.4.4.

While Proposition 1 is all we need to ensure we can harvest all previously established results on PLRNNs in particular, and on continuous PWL maps more generally, it is revealing to note that any dendPLRNN (Eqs. 1, 4) can be rewritten as a conventional PLRNN, as stated in the following theorem:

**Theorem 1.** Any $M$-dimensional dendPLRNN as defined in Eqs. 1, 4, can always be rewritten as a $M \times B$-dimensional “conventional” PLRNN of the form

$$\dot{z}_t = A \dot{z}_{t-1} + \tilde{W} \max(0, \dot{z}_{t-1}) + \tilde{h}_0 + \tilde{C} s_t + \tilde{e}_t.$$  

(5)

**Proof.** Straightforward by construction, see Appx. 6.4.5. 

This theorem highlights why the dendPLRNN will allow to reduce the dimensionality of the reconstructed system, as it suggests we may often be able to reformulate a high-dimensional PLRNN in terms of an equally powerful lower-dimensional dendPLRNN. In Appx. 6.4.1 we also spell out the exact computation of fixed points and $k$-cycles for the dendPLRNN.

Finally, the unboundedness of the PLRNN’s latent states due to the ReLU function can cause divergence problems in training. The dendPLRNN, on the other hand, offers a simple and natural way to contain the latent states without violating the basic model description above, as established in the following theorem:

**Theorem 2.** For each basis $\{\alpha, h_b\}$ in Eq. 4 of a dendPLRNN let us add another basis $\{\alpha^*_b, h^*_b\}$ with $\alpha^*_b = -\alpha_b$ and $h^*_b = 0$. Then, for $\sigma_{\text{max}}(A) < 1$, any orbit of this “clipped” dendPLRNN (Eq. 10) will remain bounded.

**Proof.** See Appx. 6.4.6. 

Appx. 6.4 collects further theoretical results, assuring, for instance, that the manifold attractor regularization employed here (see next section) does not interfere with the results above (Proposition 2).

### 3.4. Training the dendPLRNN

We apply two different training strategies to infer the parameters $\theta = \{A, W, h, C, \Sigma, B, \Gamma, \{\alpha, h_b\}\}$ of the dendPLRNN (Eq. 1, 3, 4) from observed data: First, we employ “classical” BPTT with a variant of TF (Williams & Zipser, 1989; Pearlmutter, 1990). TF here means that the first $N$
latent states $z_{k,l\tau +1}, k \leq N$, were replaced by observations $x_{k,l\tau +1}$ at times $l\tau +1, l \in \mathbb{N}_0$, where $\tau \geq 1$ is the forcing interval (for details, see Appx. 6.1). Second, we use a fast and scalable variational inference (VI) algorithm which maximizes the Evidence Lower Bound (ELBO) $\mathcal{L}(\theta, \phi; x) := \mathbb{E}_q[\log(p(x|z))] - KL[q(z|x)||p_0(z)]$ using the reparametrization trick (Kingma & Welling, 2014), and convolutional neural networks (CNNs) for parameterizing the encoder model $q(z|x)$ (see Appx. 6.1 for details). Furthermore, as proposed in Schmidt et al. (2021), to efficiently capture DS at multiple time scales, for VI we add a regularization term to the ELBO that encourages the mapping of slow time constants and long-range dependencies (so-called manifold attractor regularization, see Eq. 6, with regularization factor $\lambda$).

4. Experiments

4.1. Performance Measures

In DS reconstruction, we aim to capture invariant properties of the underlying DS like its geometrical and temporal structure. To evaluate the quality of reconstructions w.r.t. geometrical properties we employed a Kullback-Leibler divergence ($D_{\text{KL}}$) that quantifies the agreement in attractor geometries (more details in Appx. 6.2), as first suggested in Koppe et al. (2019) (see also Schmidt et al. (2021)). Specifically, this measure evaluates the overlap between the observed data distribution $p(x^{\text{obs}})$ and the distribution $p(x^{\text{gen}}|z^{\text{gen}})$ generated from model simulations (i.e., with $z^{\text{gen}} \sim p_0(z)$ after model training) across state space (not time!). Since this measure as originally defined in Koppe et al. (2019) is expensive to compute, for the high-dimensional benchmark DS we used another approximation, details of which are given in Appx. 6.2. $D_{\text{KL}}$ is evaluated on a test set of 100 trajectories with randomly sampled initial conditions and 1000 time steps each. To assess the agreement in temporal structure, power spectra were first computed through the Fast Fourier Transform (Cooley & Tukey, 1965) on all dimensions (i.e., time series) and slightly smoothed with Gaussian kernels to remove noise. For each dimension, the power spectral correlation (PSC) between ground truth and model-generated time series was then computed and averaged across dimensions (see Appx. 6.2). Finally, we also computed a 20-step-ahead prediction error along test set trajectories to assess short-term behavior (see Appx. 6.2). We note, however, that prediction errors can be misleading in case of chaotic systems because of exponential trajectory divergence, as illustrated in Koppe et al. (2019) (i.e., may be large even if the true system has been accurately captured, and vice versa). They therefore need to be interpreted with caution and are less relevant in the context of DS reconstruction than the statistics introduced above.

4.2. DS Benchmarks Used for Evaluation

We evaluated our approach and the specific role of the basis expansion on six different types of challenging DS benchmarks.

First, the famous 3d chaotic Lorenz attractor (Lorenz-63) originally proposed by Lorenz (1963) (formally defined in Appx. 6.3) has become a popular benchmark for DS reconstruction algorithms. Fig. 2a (l.h.s.) illustrates true (blue) and reconstructed (orange) time series from this system, while the r.h.s. illustrates the chaotic attractor’s geometry in its 3d state space for both the ground truth (blue) and reconstructed (orange) systems. It is important to note that both the time and state space graphs are not merely ahead predictions from the dendPLRNN but are produced by simulating the trained dendPLRNN from some initial condition. This illustrates that the dendPLRNN has captured the temporal and geometrical structure of the original Lorenz-63 system in its own governing equations. Moreover, computing analytically (see Appx. 6.4.1) the fixed points of the reconstructed system, we see that their positions in state space agree well with those of the true system.

Second, a 3d biophysical model of a bursting neuron (see Eq. 15 in Appx. 6.3; Durstewitz (2009)) highlights another aspect of DS reconstruction: Besides an equation for membrane voltage ($V$), the model consists of one very fast ($n$) and one slow ($h$) variable that control the gating of the model’s ionic conductances. This produces fast spikes that ride on top of a much slower oscillation, making this system challenging to reconstruct. One such successful dendPLRNN reconstruction is illustrated in Fig. 2b (orange) together with time graphs and state space representations of the true system (blue).

Third, the Lorenz-96 weather model is an example of a higher-dimensional, spatially organized chaotic system with local neighborhood interactions that can be extended to arbitrary dimensionality (Eq. 18 in Appx. 6.3). It has also been used more widely for benchmarking DS reconstruction algorithms. For our experiments we employed a 10-dimensional spatial layout. Fig. 3a illustrates time graphs for selected dimensions (top), the full evolving spatio-temporal pattern (center), and examples of power spectra (bottom) for both the ground truth system (blue) and an example reconstruction (orange). The spatio-temporal characteristics of the true and the dendPLRNN-generated time series tightly agree.

Fourth, as another high-dimensional example we used a neural population model with structured connectivity tuned to produce coherent chaos (Landau & Sompolinsky, 2018), from which we produced 50d observations (see Appx. 6.3 for details). Fig. 3b provides example time series (top),
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Figure 2. Examples of low-dimensional model reconstructions: (a) Time series (left) and state space trajectories (right) for the original Lorenz-63 chaotic attractor and simulations produced by a dendPLRNN trained with VI ($B = 20$, $M = 15$, $\lambda = 1.0$, $M_{reg}/M = 0.5$). Dots indicate true and reconstructed fixed points. (b) Same for the bursting neuron model, produced by a dendPLRNN trained with TF ($B = 47$, $M = 26$, $\tau = 5$). Note that the bursting is a complex limit cycle but non-chaotic.

Figure 3. Examples of high-dimensional model reconstructions: (a) Time series (top), spatio-temporal evolution (middle), and power spectra (bottom) for the true 10d Lorenz-96 system and for dendPLRNN simulations ($B = 50$, $M = 30$, $\tau = 10$). (b) Same for a 50d neural population model producing coherent chaos ($B = 5$, $M = 12$, $\lambda = 1.0$, $M_{reg}/M = 0.2$).

4.3. Basis Expansion Allows for Reduced Dimensionality

Fig. 4 shows the reconstruction performance of the dendPLRNN on the Lorenz-63 DS when trained with a range of different numbers of bases $B$ and latent states $M$. As conjectured in Sec. 3 and confirmed by these results, the latent space dimensionality $M$ can indeed be reduced profoundly, at no loss in geometrical reconstruction quality (as assessed by $D_{step}$), by increasing the expansion order $B$.

full spatio-temporal patterns (center), and overlaid power spectra (bottom) for time series drawn from the true system (blue) and those simulated by a trained dendPLRNN (orange). Again there is a tight agreement, and again we emphasize that - like in all the other examples - these are not mere model ahead-predictions but fully simulated from some random initial condition.

Finally, we studied two real-world datasets consisting of electroencephalogram (EEG) recordings from human subjects, described in more detail with results (Fig. S4) in Appx. 6.3, and an electrocardiogram (ECG), recorded from a human subject with a chest sensor (Fig. S5), described in more detail in Appx. 6.3.

4.4. Model Comparisons

We compared our model to the PLRNN without dendritic expansion and four other algorithms purpose-tailored for DS reconstruction: First, SINDy (Brunton et al., 2016) aims to reconstruct the governing equations by approximating numerical derivatives (obtained by differencing the time series, and applying a variance regularization to reduce noise) through a large library of (usually polynomial) basis functions. Sparse (LASSO) regression is used to pick out the right terms from the library (we used the PySINDy implementation (de Silva et al., 2020) with multinomials up to sixth order). Second, Vlachas et al. (2018) used a hybrid of LSTMs, trained using truncated BPTT, and mean-field stochastic models based on Ornstein-Uhlenbeck processes (LSTM-MSM) to approximate the true system’s vector field estimated from observed time series. Third, Pathak et al. (2018) built on reservoir computing (RC) for their approach with reservoir parameters chosen to satisfy the “echo state property” (Jaeger & Haas, 2004). For high-dimensional systems, a spatially arranged set of reservoirs with local neighborhood relations is employed. Fourth, Neural-ODEs (Chen et al., 2018) were trained based on an implementation in the torchdiffeq package using the odeintadjoint method for the backward pass. For all these systems, we performed grid searches for optimal
we tried to ensure roughly the same number of trainable (see Appx. 6.3 for further methodological details). To produce this table, 100,000 time steps for both training and testing were simulated from each ground truth system, all dimensions were standardized to have zero mean and unit variance, and process noise and observation noise (with about 1% of the data variance) were added while simulating the (now stochastic) differential equations, and after drawing the observations, respectively (see Appx. 6.3 for further methodological details). To produce statistics, each method was run from a total of 20 randomly chosen initial conditions for the parameters. We also tested all five methods on-real-world EEG and ECG data and on challenging data situations produced using the Lorenz-63 system (Fig. 2a), with either short time series of just 1000 time steps for training, only partial observations (just state variable $x$ in Eq. 14 in Appx. 6.3), or high process and high observation noise (drawing from a Gaussian with $dε \sim N(0, 0.1 dt \times I)$ for the process noise as described in Appx. 6.3, and using 10% of the observation variance, respectively). SINDy cannot naturally handle missing observations, as it has no latent variables but formulates the model directly in terms of the observations. Therefore, for the partially observed system, we used a delay embedding (Takens, 1981; Sauer et al., 1991) to create a 3d dataset, adding two time-lagged versions of $x$ as coordinates.\(^4\)

A general observation is that indeed all five models are quite powerful for reconstructing the underlying DS. However, in most comparisons the dendPLRNN had an edge over the other methods, or came out second after SINDy, especially when trained by BPTT+TF (see Appx. S2 for results obtained with VI). SINDy tends to outperform the dendPLRNN on the Lorenz-63 DS, but it performs poorly on the bursting neuron example and fails on the neural population model, as well as on the EEG and ECG data. It also becomes comparatively slow to train on high-dimensional systems (as the number of bases needed scales exponentially with the number of dimensions). This can be explained by the fact that SINDy already has the correct functional form for the Lorenz-63 (and also Lorenz-96) DS: Both of these have a strictly polynomial form (see Eq. 14 and Eq. 18 in Appx. 6.3), and SINDy (in our tests) works with a set of polynomial library functions to begin with. Hence, SINDy only needs to pick out the right terms from its expansion to succeed, giving it a clear advantage on these model systems by design. On the other hand, as indicated in Table 1, it largely fails on systems which have a different (in this case non-polynomial) functional form, or when the true form, as in the EEG and ECG empirical examples, is simply not known. Unlike the other methods, SINDy therefore appears less suitable as a general framework for DS reconstruction if an appropriate library of basis functions cannot be specified a priori, a potential shortcoming already discussed by the original authors (Brunton et al., 2016).

While our conclusion is that essentially all of the four tested models LSTM-MSM, RC, Neural ODE and dendPLRNN, are suitable for reconstruction of arbitrary unknown DS, even in very challenging data situations (Table 1, bottom),

\(^4\)Note that SINDy by design always has as many dynamical variables as observed (or embedded) dimensions. This could be an advantage if the observed system really is that low-dimensional. If, however, the number of observations is much larger than those needed to describe the generating DS (as often suspected in neuroscience) or – vice versa – not all system states have been observed, SINDy may need to be augmented by other techniques (see Champion et al. (2019); Bakarji et al. (2022)).
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LSTM-MSM, RC and Neural-ODE performed worse on average and have other disadvantages compared to our method: First, they are quite complex in their architectures and hence not easily interpretable, i.e. much harder to track and analyze mathematically. In contrast, as summarized in Sec. 3.3, the dendPLRNN is a continuous PWL map and as such comes with a huge bulk of already existing theoretical results (Schmidt et al., 2021; Monfared & Durstewitz, 2020a;b), as well as with mathematical tractability. This aspect is illustrated more explicitly in Fig. 5 which shows true and reconstructed vector fields and fixed point locations of what precisely is learnt in terms of dynamics if the reservoirs themselves cannot adapt to the DS at hand.

| Dataset       | Method      | PSC       | $D_{top}$       | 20-step PE | Dyn.var | #parameters |
|---------------|-------------|-----------|----------------|------------|---------|-------------|
| Lorenz-63     | dendPLRNN TF| 0.997 ± 0.002 | 0.13 ± 0.18 | 9.2e−5 ± 2.8e−5 | 22      | 1032        |
|               | RC          | 0.991 ± 0.001 | 0.24 ± 0.05 | 1.2e−2 ± 0.1e−3 | 345     | 1053        |
|               | LSTM-MSM    | 0.985 ± 0.004 | 0.85 ± 0.07 | 1.2e−2 ± 0.1e−3 | 29      | 1035        |
|               | SINDy       | 0.998 ± 0.0003 | 0.04 ± 0.01 | 6.8e−5 ± 0.2e−5 | 3       | 252         |
|               | Neural ODE  | 0.992 ± 0.001 | 0.149 ± 0.014 | 1.1e−3 ± 4.1e−5 | 3       | 1011        |
| Bursting Neuron| dendPLRNN TF| 0.76 ± 0.04 | 0.61 ± 0.09 | 6.1e−2 ± 2.2e−2 | 26      | 2040        |
|               | RC          | 0.51 ± 0.01 | 5.1 ± 0.6 | 8.6e−2 ± 0.1e−2 | 711     | 2133        |
|               | LSTM-MSM    | 0.54 ± 0.02 | 2.83 ± 0.36 | 3.9e−2 ± 0.1e−2 | 45      | 2166        |
|               | SINDy       | 0.25 ± 0.01 | 6.36 ± 0.02 | 5.4e−1 ± 0.1e−2 | 3       | 252         |
|               | Neural ODE  | 0.65 ± 0.017 | 3.85 ± 0.1 | 2.1e−1 ± 0.5e−2 | 3       | 2073        |
| Lorenz-96     | dendPLRNN TF| 0.998 ± 0.0001 | 0.04 ± 0.01 | 4.1e−2 ± 0.8e−2 | 50      | 4480        |
|               | RC          | 0.986 ± 0.008 | 0.25 ± 0.17 | 7.1e−1 ± 0.1e−2 | 440     | 4400        |
|               | LSTM-MSM    | 0.993 ± 0.002 | 0.23 ± 0.03 | 8.2e−1 ± 0.3e−2 | 62      | 4384        |
|               | SINDy       | 0.997 ± 0.001 | 0.06 ± 0.003 | 6.3e−2 ± 0.1e−2 | 10      | 27410       |
|               | Neural ODE  | 0.985 ± 0.001 | 0.21 ± 0.02 | 4.4e−2 ± 4.5e−2 | 10      | 4130        |
| Neural Pop. Model | dendPLRNN TF| 0.52 ± 0.01 | 0.37 ± 0.05 | 1.43 ± 0.01 | 75      | 9990        |
|               | RC          | 0.34 ± 0.03 | 2.8 ± 0.4 | 1.64 ± 0.07 | 200     | 10090       |
|               | LSTM-MSM    | 0.51 ± 0.02 | 0.29 ± 0.04 | 1.56 ± 0.01 | 56      | 10298       |
|               | SINDy       | diverging  | diverging     | diverging   | 50      | 66300       |
|               | Neural ODE  | 0.47 ± 0.03 | 9.56 ± 0.86 | 0.58 ± 0.006 | 50      | 10200       |
| EEG           | dendPLRNN TF| 0.923 ± 0.012 | 1.96 ± 0.18 | 0.202 ± 0.007 | 128     | 27058       |
|               | RC          | 0.782 ± 0.002 | 8.8 ± 0.8 | 0.78 ± 0.02 | 448     | 28672       |
|               | LSTM-MSM    | 0.827 ± 0.002 | 8.3 ± 0.3 | 0.708 ± 0.003 | 168     | 27728       |
|               | SINDy       | diverging  | diverging     | diverging   | 64      | 133120      |
|               | Neural ODE  | 0.82 ± 0.002 | 21.72 ± 0.71 | 0.31 ± 0.005 | 64      | 30559       |
| ECG           | dendPLRNN TF| 0.920 ± 0.014 | 0.4 ± 0.6 | 0.23 ± 0.03 | 30      | 2641        |
|               | RC          | 0.880 ± 0.013 | 1.78 ± 0.44 | 0.571 ± 0.013 | 378     | 2646        |
|               | LSTM-MSM    | 0.926 ± 0.007 | 0.59 ± 0.08 | 7.0e−2 ± 0.6e−2 | 51      | 2801        |
|               | SINDy       | diverging  | diverging     | diverging   | 7       | 4424        |
|               | Neural ODE  | 0.90 ± 0.011 | 1.18 ± 0.02 | 0.61 ± 0.01 | 7       | 2599        |
| Low amount of data | dendPLRNN TF| 0.97 ± 0.04 | 6.9 ± 5.3 | 1.5e−2 ± 0.9e−2 | 22      | 1032        |
|               | RC          | 0.68 ± 0.05 | 5.74 ± 0.11 | 4.1e+5 ± 1.2e+5 | 345     | 1053        |
|               | LSTM-MSM    | 0.960 ± 0.006 | 6.06 ± 0.37 | 2.1e−1 ± 0.3e−2 | 29      | 1035        |
|               | SINDy       | 0.998 ± 0.0003 | 0.04 ± 0.01 | 6.8e−5 ± 0.2e−5 | 3       | 252         |
|               | Neural ODE  | 0.967 ± 0.008 | 4.66 ± 0.31 | 1.6e−3 ± 1.8e−4 | 3       | 1011        |
| Partially observed | dendPLRNN TF| 0.993 ± 0.003 | 0.54 ± 0.16 | 5.3e−3 ± 0.2e−3 | 22      | 1032        |
|               | RC          | 0.981 ± 0.001 | 2.92 ± 0.08 | 7.6e−3 ± 0.1e−3 | 345     | 1053        |
|               | LSTM-MSM    | 0.934 ± 0.005 | 6.06 ± 0.37 | 2.3e−2 ± 0.3e−2 | 29      | 1035        |
|               | SINDy       | 0.974 ± 0.001 | 2.52 ± 0.01 | 7.4e−3 ± 0.1e−3 | 3       | 252         |
|               | Neural ODE  | 0.945 ± 0.004 | 3.34 ± 0.12 | 8.3e−3 ± 9e−5 | 3       | 1011        |
| High noise    | dendPLRNN TF| 0.995 ± 0.002 | 0.4 ± 0.13 | 4.6e−3 ± 0.4e−3 | 22      | 1032        |
|               | RC          | 0.988 ± 0.001 | 2.35 ± 0.21 | 3.1e−2 ± 0.2e−2 | 345     | 1053        |
|               | LSTM-MSM    | 0.967 ± 0.006 | 1.19 ± 0.27 | 3.5e−2 ± 0.2e−2 | 29      | 1035        |
|               | SINDy       | 0.984 ± 0.005 | 0.42 ± 0.01 | 7.0e−3 ± 0.1e−4 | 3       | 252         |
|               | Neural ODE  | 0.982 ± 0.055 | 0.79 ± 0.06 | 5.5e−3 ± 1.7e−4 | 3       | 1011        |
for the Wilson-Cowan model of neural population dynamics (see Appx. 6.3) in the bistable regime. Fixed points were computed analytically for the dendPLRNN (cf. also Fig. 2a and Appx. 6.4.1), and match those of the ground truth system both in position and stability as determined from the dendPLRNN’s Jacobian. On top, the dendPLRNN mostly achieves reconstructions of the DS in (much) lower dimensions than RC or LSTM-MSM (see Table 1), further adding to its better interpretability. By embedding the dendPLRNN within a SVAE (Archer et al., 2015) framework (see Appx. 6.1), one could also obtain uncertainty estimates on the state trajectories and perform posterior inference, features that the other models lack.

5. Conclusions

In this work we augmented PLRNNs (Durstewitz, 2017; Koppe et al., 2019) by a linear spline basis expansion inspired by principles of dendritic computation. We show mathematically that by doing so we remain within the theoretical framework of continuous PWL maps and hence can harvest a huge bulk of existing DS theory (Sec. 3.3), while at the same time achieving better performance with less parameters and in lower dimensions. This is a key advantage from a scientific perspective where mechanistic insight and understanding of the system under study is sought. Indeed, we are not aware of any other current DS reconstruction approach that combines these features, a simple, mathematically tractable design with competitive performance, yet providing comparatively low-dimensional representations of the dynamics. Another contribution of the present work is that it assembles a set of DS benchmarks, experimental settings, and reconstruction measures which may be helpful more generally for assessing DS reconstruction algorithms, including an extension of a geometrical reconstruction measure ($D_{met}$) for use in high dimensions.

Using a stochastic latent model and VI/SVAE for training (see Appx. 6.1) in addition yields posterior distributions and uncertainty estimates across latent state trajectories. Somewhat surprisingly, however, the BPTT+TF approach to model training clearly outperformed the more sophisticated VI approach (see Table S2). This could be rooted in suboptimal encoder models or, as we suspect, in suboptimal sampling from the approximate posterior: BPTT+TF (and, similarly, LSTM-MSM) allow trajectories to evolve freely for several time steps during training and hence assess longer bits of trajectory for optimization. In contrast, in VI single time points are sampled separately from the approximate posterior and overall temporal consistency is ensured only through the Kullback-Leibler term in the ELBO. Other more expressive yet still fast to compute encoder models that better map a trajectory’s temporal evolution, e.g., based on normalizing flows (Rezende & Mohamed, 2015), may boost performance. Specific annealing and curriculum training protocols (as used in Koppe et al. (2019)) are other amendments to consider.

Another potentially interesting direction would be to augment the model with multiple trainable and adaptive time scales, as in LEM networks (Rusch et al., 2022). While this is similar in spirit to the manifold attractor regularization scheme proposed for PLRNNs by Schmidt et al. (2021) (see also Fig. S1), LEMs allow for a more flexible and state/input-dependent way of adjusting the system’s time constants. In preliminary studies we observed LEM networks to come close to our model for DS reconstruction tasks. Borrowing LEM’s basic functional principles while retaining the dendPLRNN’s tractable form thus appears to be another promising though challenging avenue.

Software and Data

All code created in here is available at https://github.com/DurstewitzLab/dendPLRNN.

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6. Appendix

6.1. Further Methodological Details

**Manifold Attractor Regularization** As proposed in Schmidt et al. (2021), to encourage the discovery of long-term dependencies and slow time scales in the data, a subset of $M_{\text{reg}} \leq M$ states was regularized by adding the following term to the ELBO for the VI approach:

$$
\mathcal{L}_{\text{reg}} = \lambda \left( \sum_{i=1}^{M_{\text{reg}}} (A_i - 1)^2 + \sum_{i=1}^{M_{\text{reg}}} \sum_{j \neq i} (W_{ij})^2 + \sum_{i=1}^{M_{\text{reg}}} h_i^2 \right). 
$$

(6)

This regularization pushes the regularized subset of states toward a continuous set of marginally stable fixed points that tends to form an attracting manifold in the full state space, which supports the learning of systems with widely differing time scales, such as the bursting neuron model (cf. Sec. 4). During training with VI, the ELBO was divided by the number of time steps $T$ of a given batch to put it on equal grounds with the regularization term. Regularization settings used are summarized in Table S1 along other hyper-parameter settings.

![Figure S1](image-url). Different latent states capture different time scales of the reconstructed DS. (a) Simulated time series of the first ($V/x_1$) and third ($h/x_3$) system variables from a reconstruction (dendPLRNN trained with BPTT, $M = 20$, $B = 20$, $\tau = 5$, $M_{\text{reg}}/M = 0.5$, $\lambda = 0.05$) of the bursting neuron model (Eq. 15). (b) Time series of the two latent states with the lowest ($a_{8,8} \approx 0.1012$, left) and highest ($a_{10,10} \approx 0.9987$, right) time constants of a dendPLRNN trained with manifold attractor regularization (MAR), capturing the fast spiking and slow oscillatory time scales of the bursting neuron, respectively. (c) Same as (b) for a dendPLRNN trained without manifold attractor regularization. In this case the separation of time scales in the latent states is often less clear, although in this particular example the lowest ($a_{7,7} \approx 0.0067$, left) and highest ($a_{18,18} \approx 0.6951$, right) time constants still tend to capture the bursting neuron’s fastest and slowest time scales, respectively. Similar observations were also made for other systems like the ECG and EEG data (not shown).

**BPTT-TF** To train a deterministic version of the dendPLRNN, we employ BPTT with a scheduled version of TF (Williams & Zipser, 1989; Pearlmutter, 1990). To do so, we choose an “identity-mapping” for the observation model $\hat{x}_t = \mathcal{I}x_t$, where $\mathcal{I} \in \mathbb{R}^{N \times M}$ with $\mathcal{I}_{kk} = 1$ if $k \leq N$ and zeroes everywhere else. This allows us to regularly replace latent states...
with observations to “recalibrate” the model and break trajectory divergence in case of chaotic dynamics. Consider a time series \(\{x_1, x_2, \cdots, x_T\}\) generated by a DS we want to reconstruct. At times \(l\tau + 1, \ l \in N_0, \) where \(\tau \geq 1\) is the forcing interval, we replace the first \(N\) latent states by observations \(\hat{z}_{k,l\tau+1} = x_{k,l\tau+1}, \ k \leq N.\) The remaining latent states, \(\hat{z}_{k,l\tau+1} = z_{k,l\tau+1}, \ k > N,\) remain unaffected by the forcing. This means that we optimize the dendPLRNN such that a subspace of the latent space directly maps to the observed time series variables. The forcing interval \(\tau\) is a hyperparameter, with optimal settings varying depending on the dataset. The settings we chose are summarized in Table S1. With \(\mathcal{F} = \{l\tau + 1\}_{l \in N_0}\), the dendPLRNN updates can then be written as

\[
\hat{z}_{t+1} = \begin{cases} 
\text{dendPLRNN}(\hat{z}_t) & \text{if } t \in \mathcal{F} \\
\text{dendPLRNN}(z_t) & \text{else} 
\end{cases} 
\tag{7}
\]

The loss is calculated prior to the forcing, such that \(\mathcal{L}_t = \|x_t - \mathcal{I} z_t\|_2^2\) for every time step. To improve performance, in some experiments we employed a mean-centered dendPLRNN (for details see next paragraph). In the evaluation phase, the trained dendPLRNN is simulated freely without any forcing. As the model is deterministic, the initial condition \(z_1 = [x_1, Lx_1]^T\) is estimated from the first data point \(x_1\) with a matrix \(L \in \mathbb{R}^{(M-N) \times N}\) which is jointly learned with the other model parameters.

**Mean-Centered dendPLRNN**  Layer normalization has recently been developed as a way of significantly improving RNN training (Ba et al., 2016). Here we adapt the idea of layer normalization to the piecewise-linear nature of our dendPLRNN. Instead of fully standardizing the latent states at every time step before applying the activation function, we only mean-center them:

\[
z_t = Az_{t-1} + W \phi(M(z_{t-1})) + h_0, \tag{8}
\]

where \(\phi(\cdot)\) is given in Eq. 4 and \(M(z_{t-1}) = z_{t-1} - \mu_{t-1} = z_{t-1} - \frac{1}{M} \sum_{j=1}^{M} z_{j,t-1},\) where \(1 \in \mathbb{R}^M\) is a vector of ones. Note that this mean-centering is linear and can be rewritten as a matrix-multiplication

\[
M(z_{t-1}) = z_{t-1} - \mu_{t-1} = \frac{1}{M} \begin{pmatrix}
M - 1 & -1 & \cdots & -1 \\
-1 & M - 1 & \cdots & -1 \\
: & : & \ddots & : \\
-1 & -1 & \cdots & M - 1
\end{pmatrix} z_{t-1} = M z_{t-1}. \tag{9}
\]

As Remark 1 points out, all results about the tractability of the dendPLRNN also hold for the mean-centred dendPLRNN.

**State Clipping**  Since the ReLU function used in the dendPLRNN is non-saturating, states may diverge to infinity. As Theorem 2 guarantees, there is a simple and natural way to construct a “clipped” dendPLRNN

\[
z_t = Az_{t-1} + W \sum_{b=1}^{B} \alpha_b \left[ \max(0, z_{t-1} - h_b) - \max(0, z_{t-1}) \right] + h_0. \tag{10}
\]

Note that the results of Theorem 2 also hold true when the manifold attractor regularization is applied. This is detailed in Proposition 2 further below.

**Approximate Posterior for Variational Inference**  To estimate the true unknown posterior \(p(z|x),\) we make a Gaussian assumption for the approximate posterior \(q_{\phi}(z|x) = \mathcal{N}(\mu_{\phi}(x), \Sigma_{\phi}(x))\), where mean and covariance are functions of the observations. Without any simplifying assumptions, the number of parameters in \(\Sigma_{\phi}(x) \in \mathbb{R}^{MT \times MT}\) would scale unacceptably with time series length \(T.\) We therefore made a mean field assumption and factorized \(q_{\phi}(z|x)\) across time. Specifically, a time-dependent mean \(\mu_{t,\phi}\) and covariance \(\Sigma_{t,\phi}\) were parameterized through stacked convolutional networks which take the observations \(\{x_{t-w}, \cdots, x_{t+w}\}\) as inputs, with \(w\) given by the largest kernel size. The mean is given by a 4-layer CNN with decreasing kernel sizes (41, 31, 21 and 11, respectively), with the last layer of the CNN feeding into the parameters of the approximate posterior. For the diagonal covariance, the observations are mapped directly onto the
logarithms of the covariance through a single convolutional layer (with a kernel size of 41) mapping onto the parameters of the approximate posterior. The classical motivation behind using CNNs rests on the assumption that the data contains translationally invariant patterns, and that this allows the recognition model to embed potentially meaningful temporal context into the latent representation (see e.g. Cui et al. (2016)). We note that while the mean-field approximation is computationally highly efficient, it makes potentially strongly simplifying assumptions (Blei et al., 2017; Bayer et al., 2021) that may limit the ability of the encoder model to approximate the true posterior. Somewhat surprisingly, the BPTT+TF approach to model training clearly outperformed the more sophisticated VI approach. This could be rooted in suboptimal encoder models or in suboptimal sampling from the approximate posterior: While BPTT+TF assesses longer bits of trajectory during optimization, in VI single time-point samples are drawn and the temporal consistency is ensured only through the Kullback-Leibler term in the ELBO. Other more expressive yet still fast to compute encoder models, e.g., based on normalizing flows (Rezende & Mohamed, 2015), may boost performance.

**Hyperparameter Setting** To train the dendPLRNN in the VI framework, Adam (Kingma & Ba, 2015), with a batch size of 1000 and learning rate of $10^{-3}$ was used as the optimizer. For the training with BPTT, we used the Adam optimizer with an initial learning rate of $10^{-3}$ that was iteratively reduced during training down to $10^{-5}$. For each epoch we randomly sampled sequences of length $T_{\text{seq}} = 500$ (except for the Lorenz-63 runs, where $T_{\text{seq}} = 200$ time steps were sufficient) from the total training data pool of each dataset, which are then fed into the reconstruction method in batches of size 16. Parameters $A$, $W$ and $h$ were initialized according to Talathi & Vartak (2016), while the $\{a_\theta\}$ were initialized according to a uniform distribution in $[-B^{-0.5}, B^{-0.5}]$. Initial thresholds $\{h_\theta\}$ also followed uniform distributions, but with ranges determined by the extent of the data, i.e. such that the whole data domain was covered. To find optimal hyper-parameters we performed a grid search within $\{\alpha \in \{0, 0.01, 0.1, 1\}\}$ (VI), $\tau \in \{1, 5, 10, 25, 50, 100\}$ (BPTT-TF), $M \in \{5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 75, 100\}$, and $B \in \{0, 1, 2, 5, 10, 20, 35, 50\}$. Hyper-parameters chosen for the benchmarks in Sec. 4 are reported in Table S1 below (note that these may not fully agree with the ranges initially scanned, as given above, since we attempted to adjust them further in order to approximately match the number of parameters among models in Table 1).

| Dataset          | M   | B      | $M_{\text{reg}}/M$ | $\lambda$ | $\tau$ |
|------------------|-----|--------|--------------------|-----------|--------|
| Lorenz-63        | 22  | 20     | 1.0/−              | 1.0/−     | −/25   |
| Lorenz-96        | 42/50 | 50/30 | 1.0/−              | 1.0/−     | −/10   |
| Bursting Neuron  | 26  | 50/47  | 0.5/−              | 1.5/−     | −/5    |
| Neural Population | 12/75 | 5/40  | 0.2/−              | 1.0/−     | −/5    |
| EEG              | 117/128 | 50/50 | 0.8/0.1            | 1.0/5 · 10^{-3} | −/10   |
| ECG              | −/30 | −/50   | −/−                | −/−       | −/10   |

**LSTM-MSM and Reservoir Computing** For the Lorenz-63 and Lorenz-96 system, hyperparameters were used according to the default settings for these specific datasets in the codebase provided at https://github.com/pvlachas/RNN-RC-Chaos. For the other datasets not previously explored by Vlachas et al. (2018) and Pathak et al. (2018), we performed a grid search to find best performing hyperparameter configurations. To this end, the following hyperparameters were scanned for the RC and LSTM-MSM approach, respectively: For RC the scanned hyperparameters and values are the $\text{dynamics.length} \in \{10, 50, 100, 200, 500\}$, $\text{noise.level} \in \{10, 100, 1000\}$, $\text{regularization} \in \{0, 10^{-1}, 10^{-2}, 10^{-3}\}$ and $\text{learning.rate} \in \{10^{-2}, 10^{-3}, 10^{-4}\}$. For LSTM-MSM, similar parameters were explored, where the equivalent of $\text{dynamics.length}$ is $\text{hidden.state.propagation.length}$ in the respective code. Also, due to the comparatively slow execution times, only fewer parameter combinations were tried.

**Neural ODE** For Neural ODEs we used the implementation in the torchdiffeq package. The number of layers was fixed to the number of trainable parameters comparable to those in Table 1, while a grid search was performed over activation functions \{elu, silu, tanh\}, sequence length \{5, 10, 25, 50\} used per batch, and learning rates \{1e−3, 1e−2\}. For each dataset, 20 models were trained for 1000 epochs, each with a batch size of 20. The odeintadjoint method with the default solver dopri5 was mostly used for training. As the adaptive step size caused numerical instabilities during training on the two experimental datasets, we switched to the solver euler for these.
For PySINDy we performed a hyperparameter search over threshold values \{0.0001, 0.0002, 0.0005, 0.001, 0.002, 0.005, 0.01, 0.02, 0.05, 0.1\} in the `stlsqoptimizer`. This threshold specifies the minimum value for a coefficient in the weight vector, below which it is dropped out (i.e., set to zero).

6.2. Performance Measures

**Geometrical Measure** $D_{\text{step}}$ used for evaluating attractor geometries (Fig. 4) measures the match between the ground truth distribution $p_{\text{true}}(x)$ and the generated distribution $p_{\text{gen}}(x \mid z)$ through the discrete binning approximation (Koppe et al., 2019)

$$D_{\text{step}}(p_{\text{true}}(x), p_{\text{gen}}(x \mid z)) \approx \sum_{k=1}^{K} \hat{p}^{(k)}(x) \log \left( \frac{\hat{p}^{(k)}(x)}{\hat{p}_{\text{true}}^{(k)}(x)} \right),$$

where $K$ is the total number of bins, and $\hat{p}_{\text{true}}^{(k)}(x)$ and $\hat{p}_{\text{gen}}^{(k)}(x \mid z)$ are estimated as relative frequencies through sampling trajectories from the benchmark DS and the trained reconstruction method, respectively. A range of $2 \times$ the data standard deviation on each dimension was partitioned into $m$ bins, yielding a total of $K = m^N$ bins, where $N$ is the dimension of the ground truth system. Initial transients are removed from sampled trajectories to ensure that the system has reached a limiting set. If the bin size is chosen too large, important geometrical details may be lost, while if it is chosen too small, noise and (low) sampling artifacts with many empty bins may misguide the approximation above. Here we chose a bin number of $m = 30$ per dimension as an optimal compromise that distinguished well between successful and poor reconstructions.

Since the number of bins needed to cover the relevant (populated) region of state space scales exponentially with the number of dimensions, for high-dimensional systems evaluating $D_{\text{step}}$ as outlined above is not feasible. We therefore resorted to an approximation of the densities based on Gaussian Mixture Models (GMMs), similar to a strategy outlined in (Koppe et al., 2019). Specifically, we approximate the true data distribution by a GMM $p_{\text{true}}(x) \approx \sum_{i=1}^{L} \mathcal{N}(x_i, \Sigma)$ with Gaussians centered on the observed data points $\{x_i\}$ and covariance $\Sigma$, which we treat as a hyperparameter that determines the granularity of the spatial resolution (similar to the bin size in Eq. 11). We can generate a likewise distribution by sampling trajectories from the trained models (or one very long trajectory) and placing Gaussians on the sampled data points, $p_{\text{gen}}(x \mid z) \approx \frac{1}{T} \sum_{i=1}^{L} \mathcal{N}(\hat{x}_i \mid z_i, \Sigma)$ (in the case of VI, rather than sampling, one could also use the model’s distributional assumptions to build this posterior across the observations). For the Kullback-Leibler divergence between two GMMs efficient approximations are at hand (Hershey & Olsen, 2007). Here we employ a Monte Carlo approximation

$$\bar{D}_{\text{step}}(p_{\text{true}}(x), p_{\text{gen}}(x \mid z)) \approx \frac{1}{n} \sum_{i=1}^{n} \log \frac{1}{1/L} \frac{1/T}{\sum_{i=1}^{T} \mathcal{N}(x^{(i)}; x_i, \Sigma)}$$

where $n$ Monte-Carlo samples $x^{(i)}$ are drawn from the GMM representing $p_{\text{true}}$. In practice, we set the covariance $\Sigma = \sigma^2 I$ equal to a scaled identity matrix, with a single hyperparameter $\sigma^2$. Scanning the range $\sigma^2 \in \{0.01, 0.02, 0.05, 0.1, 0.2, 0.5, 1, 2, 5\}$, we found that values for $\sigma^2 = 0.1 – 1.0$ to differentiate best between good and bad reconstructions. We chose $\sigma^2 = 1.0$ for numerical stability. For this setting, $D_{\text{step}}$ as derived with the binning method and $\bar{D}_{\text{step}}$ computed through the GMMs also correlated highly on the low-dimensional benchmark systems (see Figure S2).

**Power Spectrum Correlation** The power spectrum correlations (PSC) were obtained by first sampling time series of 100,000 time steps, standardizing these, and computing dimension-wise Fast Fourier Transforms (using `scipy.fft`) for both the ground truth systems and model-simulated time series. Individual power spectra were then slightly smoothed with a Gaussian kernel, normalized, and the long, high-frequency tails of the spectra, mainly representing noise, were cut off. Smoothing width $\sigma$ and cutoff values were increased linearly with the length of the time series used to compute the spectrum, and were chosen by visual inspection of the individual spectra. Dimension-wise correlations between smoothed power spectra were then averaged to obtain the reported PSC scores.

**Mean Squared Prediction Error** A mean squared prediction error (PE) was computed across test sets of length $T = 1000$ by initializing the reconstructed model with the test set time series up to some time point $t$, from where it was then iterated forward by $n$ time steps to yield a prediction at time step $t + n$. The $n$-step ahead prediction error (PE) is then defined as the
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Figure S2. Correlation between the binning approximation ($m = 30$) and the logarithm of the GMM approximation ($\sigma^2 = 1$) to $D_{stsp}$ on the Lorenz-63 system for different noise realizations and variances. Similar as reported for the $KL_Z$ approximation in (Koppe et al., 2019) we observed a logarithmic relation between the GMM and binning based measures.

Figure S3. Example power spectra for different values of the smoothing factor $\sigma$.

MSE between predicted and true observations:

$$PE(n) = \frac{1}{N(T - n)} \sum_{t=1}^{T-n} \sum_{i=1}^{N} (x_{i,t+n} - \hat{x}_{i,t+n})^2.$$ (13)

Note that for a chaotic system initially close trajectories will exponentially diverge, such that PEs for too large prediction steps $n$ are not meaningful anymore (in a chaotic system with noise, for large $n$ the PE may be high even when estimated from two different runs of the same ground truth model from the same initial condition; see (Koppe et al., 2019)). How quickly this happens depends on the rate of exponential divergence as quantified through the system’s maximal Lyapunov exponent (Kantz & Schreiber, 2004).

6.3. Details on Dynamical Systems Benchmarks

Lorenz-63 System The famous 3d chaotic Lorenz attractor with the butterfly wing shape, originally proposed in (Lorenz, 1963), is defined by
We borrowed parameter settings from Schmidt et al. (2021) to place the system into the burst-firing regime: 

\[
\begin{align*}
dx &= (\sigma(y - x))dt + d\epsilon_1(t), \\
dy &= (x(\rho - z) - y)dt + d\epsilon_2(t), \\
dz &= (xy - \beta z)dt + d\epsilon_3(t).
\end{align*}
\] (14)

Parameters used for producing ground truth data in the chaotic regime were \(\sigma = 10, \rho = 28,\) and \(\beta = 8/3.\) Process noise was injected into the system by drawing from a Gaussian term \(d\epsilon \sim \mathcal{N}(0, 0.01^2 dt \times I).\)

**Bursting Neuron Model** The 3d biophysical bursting neuron model was introduced in (Durstewitz, 2009) and is defined by one voltage and two ion channel gating variables (one slow and one fast):

\[
-C_m \dot{V} = g_L (V - E_L) + g_{Na} m_\infty(V) (V - E_{Na}) \\
+ g_K n(V - E_K) + g_M h(V - E_K) \\
+ g_{NMDA} \left[ 1 + .33e^{-0.625V} \right]^{-1} (V - E_{NMDA})
\]

\[
\dot{n} = \frac{n_\infty(V) - n}{\tau_n} \\
\dot{h} = \frac{h_\infty(V) - h}{\tau_h}
\] (15) (16)

The limiting values of the ionic gates are given by

\[\{m_\infty, n_\infty, h_\infty\} = \left[ 1 + e^{(V_{Na},V_{K},V_{NMDA}) - V}/\{k_{Na},k_{K},k_{NMDA}\}\right]^{-1} .\] (17)

We borrowed parameter settings from Schmidt et al. (2021) to place the system into the burst-firing regime:

\[
C_m = 6 \mu F, g_L = 8 mS, E_L = -80 mV, g_{Na} = 20 mS, E_{Na} = 60 mV, V_{Na} = -20 mV, \\
k_{Na} = 15, g_K = 10 mS, E_K = -90 mV, V_{hK} = -25 mV, k_{K} = 5, \tau_{n} = 1 ms, g_{M} = 25 mS \\
V_{hM} = -15 mV, k_{M} = 5, \tau_{h} = 200 ms, g_{NMDA} = 10.2 mS
\]

**Lorenz-96 System** The Lorenz-96 is a high-dimensional, spatially extended weather model, also introduced by Edward Lorenz (Lorenz, 1996):

\[
\begin{align*}
\frac{dx_i}{dt} &= ((x_{i+1} - x_{i-2})x_{i-1} - x_i + F)dt + d\epsilon, \ i = 1 \ldots N,
\end{align*}
\] (18)

with (constant) forcing term \(F. F = 8\) is a common choice that leads to chaotic behavior. Process noise was added as for the Lorenz-63 system, \(d\epsilon \sim \mathcal{N}(0, 0.01^2 dt \times I).\) In our simulations we used \(N = 10,\) but in principle the system allows for arbitrary dimensionality.

**Neural Population Model** A larger-scale neural population model was recently introduced in Landau & Sompolinsky (2018) to examine the effect of structured connectivity on top of a randomly initialized network matrix. Specifically, an independently Gaussian distributed weight structure was combined with a rank-1 component with coupling strength \(J_1.\) The dynamics of the single unit currents were defined as

\[
\frac{dh}{dt} = -h + J \frac{\phi(h)}{\sqrt{N}} + J_1 \xi v^T \phi(h),
\]

where \(\phi(h) = \tanh(h(t)).\) We produced a 50-dimensional chaotic network model based on the code provided in Landau & Sompolinsky (2018) using \(J_1 = 0.09\) and seeding the random number generator with 35.

The Lorenz-63 and Lorenz-96 systems were simulated using scipy.integrate, while for the bursting neuron and neural population model we used the code provided in Schmidt et al. (2021) and Landau & Sompolinsky (2018), respectively.
We chose parameters that placed the model into a bistable regime: where signals were captured using a chest-worn device (RespiBAN Professional) with a sampling rate of 700 Hz. For the benchmark Electrocardiogram (ECG) time series were taken from the PPG-DaLiA dataset (Reiss et al., 2019). ECG signals were captured using a chest-worn device (RespiBAN Professional) with a sampling rate of 700 Hz. For the benchmark EEG Dataset Electroencephalogram (EEG) data were taken from a study by (Schalk et al., 2000) available at https://physionet.org/content/eegmmidb/1.0.0/. For simulating the model, we used the implementation provided at https://github.com/OpenSourceBrain/

Wilson Cowan Model The Wilson-Cowan model is a classical model of neural population dynamics that describes the interactions between a pool of excitatory (E) cells and one of inhibitory (I) cells (Wilson & Cowan, 1972), defined by

\[ \tau_e \frac{dx}{dt} = -x + \phi(w_{ei} \cdot r_e - w_{ie} \cdot r_i - z_e) \]

\[ \tau_i \frac{dx}{dt} = -i + \phi(w_{ei} \cdot r_e - w_{ie} \cdot r_i - z_i) \]

where \( w_{ei}, w_{ee}, w_{ie}, w_{ii} \) are coupling strengths, \( z_i \) and \( z_e \) denote constant input currents, and \( \tau_i \) and \( \tau_e \) are time constants. We chose parameters that placed the model into a bistable regime: \( w_{ei} = 9, w_{ee} = 9, w_{ie} = 5, w_{ii} = 5, z_e = 3, z_i = 4 \). The vector field and fixed points for this configuration are shown in Figure 5.

For simulating the model, we used the implementation provided at https://github.com/OpenSourceBrain/WilsonCowan. For training the dendPLRNN, we sampled 400 initial conditions evenly distributed across the unit square [0, 1]², and then simulated trajectories of \( T = 300 \) from each of these initial states. Vector fields for the dendPLRNN were approximated as finite 1-step difference vectors \( F(x_n) - x_n \) at each grid point \( x_n \), where \( F \) denotes the map induced by the dendPLRNN in observation space. Approximated and ground truth vector fields are shown in Figure 5.

EEG Dataset Electroencephalogram (EEG) data were taken from a study by (Schalk et al., 2000) available at https://physionet.org/content/eegmmidb/1.0.0/. These are 64-channel EEG data obtained from human subjects during different motor and imagery tasks. We trained the dendPLRNN using BPTT+TF on the "eyes open" baseline time series from subject 0, which had a total of 9760 time steps. The signal was standardized and smoothed with a Hann function, using numpy.hanning and a window length of 15. Results for ground-truth and freely generated EEG signals from several brain regions are shown in Figure S4.

ECG Dataset Electrocardiogram (ECG) time series were taken from the PPG-DaLiA dataset (Reiss et al., 2019). ECG signals were captured using a chest-worn device (RespiBAN Professional) with a sampling rate of 700 Hz. For the benchmark
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Figure S4. EEG recordings from frontal, occipital, parietal and temporal lobe vs. freely generated trajectories, sampled from the dendPLRNN, trained with BPTT ($M = 128$, $B = 50$, $\tau = 10$, $M_{\text{reg}}/M = 0.1$, $\lambda = 5 \cdot 10^{-3}$).

For model comparisons (Table 1), we used the first (one-dimensional) time series (index 0, “sitting”) from subject 2, which consists of 419,973 time steps. We preprocessed the data by slightly smoothing the series using a Gaussian kernel ($\sigma = 5$ time bins), standardization, and performing a temporal delay embedding with dimension $m = 7$ and lag $\tau_{\text{lag}} = 61$. Optimal embedding parameters were determined using the DynamicalSystems.jl Julia package. For the experiments, we constructed a training and test set, each of length $T = 100,000$ cut out from the available series.

Figure S5. Original ECG recording vs. freely generated time series simulated using a dendPLRNN, trained with BPTT-TF ($M = 30$, $B = 50$, $\tau = 10$).
6.4. Theoretical Analysis

Consider the PLRNN with linear spline basis expansion as defined by Eq. 1, Eq. 4, reproduced here for convenience:

\[ z_t = A z_{t-1} + W \sum_{b=1}^{B} \alpha_b \max(0, z_{t-1} - h_b) + h_0 + C s_t + \epsilon_t, \]

(22)

where \( \epsilon_t \sim \mathcal{N}(0, \Sigma), \quad E[\epsilon_t, \epsilon_t'] = 0 \) for \( t \neq t' \), \( \alpha_b \in \mathbb{R} \) are scalar weighting factors and \( h_b \in \mathbb{R}^M \) different ReLU “activation thresholds”, and all other parameters are as in conventional PLRNNs (Koppe et al., 2019).

Defining

\[ D^{(b)}_{\Omega(t-1)}(z_{t-1} - h_b) := \max(0, z_{t-1} - h_b), \]

(23)

Eq. 22 can be rewritten as

\[
\begin{align*}
\dot{z}_t &= \left( A + W \sum_{b=1}^{B} \alpha_b D^{(b)}_{\Omega(t-1)} \right) z_{t-1} \\
&\quad + W \sum_{b=1}^{B} \alpha_b D^{(b)}_{\Omega(t-1)} (-h_b) + h_0 + C s_t + \epsilon_t,
\end{align*}
\]

(24)

where \( D^{(b)}_{\Omega(t-1)} = \text{diag}(d^{(b)}_{1,t-1}, d^{(b)}_{2,t-1}, \cdots, d^{(b)}_{M,t-1}) \) are diagonal binary indicator matrices with \( d^{(b)}_{m,t-1} = 1 \) if \( z_{m,t-1} > h_{m,b} \) and 0 otherwise.

### 6.4.1. Fixed Points and \( n \)-Cycles of System Eq. 24

Defining

\[
\begin{align*}
D^B_{\Omega(t-1)} &:= \sum_{b=1}^{B} \alpha_b D^{(b)}_{\Omega(t-1)}, \\
B_{\Omega(t-1)} &:= \sum_{b=1}^{B} \alpha_b D^{(b)}_{\Omega(t-1)} (-h_b), \\
W^B_{\Omega(t-1)} &:= A + WD^B_{\Omega(t-1)},
\end{align*}
\]

(25)

and considering the autonomous system (i.e., without external inputs or noise terms), Eq. 24 can be rewritten as

\[
z_t = W^B_{\Omega(t-1)} z_{t-1} + W B_{\Omega(t-1)} + h_0.
\]

(26)

Fixed points and cycles of Eq. 22, and their eigenvalue spectra, can now be computed in a way analogous to standard PLRNNs. Specifically, solving the equation \( F(Z^{*1}) = Z^{*1} \), fixed points of the dendPLRNN are given by

\[
z^{*1} = \left( I - W^B_{\Omega(t-1)} \right)^{-1} \left[ W B_{\Omega(t-1)} + h_0 \right],
\]

(27)

where \( z^{*1} = z_{t^{*1}} = z_{t^{*1},-1} \), and \( \det(I - W^B_{\Omega(t^{*1})}) = P_{W^B_{\Omega(t^{*1})}}(1) \neq 0 \), i.e. \( W^B_{\Omega(t^{*1})} \) has no eigenvalue equal to 1. If there are eigenvalues close or equal to 1 (such that the matrix in (27) is non-invertible or badly conditioned), this means the system is undergoing a bifurcation or has one or more directions of marginal stability in its state space (e.g., may exhibit a line, plane, or manifold attractor if there is convergence to this object along the other directions). We emphasize that non-invertibility is thus not a ‘problem’ for the method, but rather indicates a dynamically important scenario in itself that can be detected from the eigenspectrum (see, e.g., Schmidt et al. (2021)).

For \( n > 1 \), an \( n \)-cycle with periodic points \( \{ z^{*n}, F(z^{*n}), F^2(z^{*n}), \cdots, F^{n-1}(z^{*n}) \} \) of map \( F \) can be obtained by solving \( F^n(z^{*1}) = z^{*1} \). Therefore, in order to find the periodic points, we first compute \( F^n \) in the following way:

\[
z_t = F(z_{t-1}) = W^B_{\Omega(t-1)} z_{t-1} + W B_{\Omega(t-1)} + h_0.
\]
$z_{t+1} = F^2(z_{t-1}) = F(z_t) = W^B_{\Omega(t)} W^B_{\Omega(t-1)} z_{t-1} + \left( W^B_{\Omega(t)} W h^B_{\Omega(t-1)} + W h^B_{\Omega(t)} \right) + (W^B_{\Omega(t)} + I) h_0,$

$z_{t+2} = F^3(z_{t-1}) = F(z_{t+1}) = W^B_{\Omega(t+1)} W^B_{\Omega(t)} z_{t-1} + \left( W^B_{\Omega(t+1)} W h^B_{\Omega(t)} + W h^B_{\Omega(t+1)} \right) + (W^B_{\Omega(t+1)} W h^B_{\Omega(t)} + W h^B_{\Omega(t+1)} + I) h_0,$

\[ \vdots \]

$z_{t+(n-1)} = F^n(z_{t-1}) = \prod_{i=2}^{n+1} W^B_{\Omega(t+n-i)} z_{t-1} + \sum_{j=2}^{n} \left[ \prod_{i=2}^{n-j+2} W^B_{\Omega(t+n-i)} W h^B_{\Omega(t+j-3)} \right] + W h^B_{\Omega(t+n-2)} + \left( \sum_{j=2}^{n} \prod_{i=2}^{n-j+2} W^B_{\Omega(t+n-i)} + I \right) h_0, \tag{28} \]

where

\[ \prod_{i=2}^{n+1} W^B_{\Omega(t+n-i)} = W^B_{\Omega(t+n-2)} W^B_{\Omega(t+n-3)} \cdots W^B_{\Omega(t-1)}. \]

Defining $t + n - 1 =: t^n$, the periodic point $z^{*n}$ of the $n$-cycle of $F$ can now be obtained as the fixed point of the $n$-times iterated map $F^n$ as

\[ z^{*n} = \left( I - \prod_{i=1}^{n} W^B_{\Omega(t^n-i)} \right)^{-1} \left[ \sum_{j=2}^{n-j+1} \left( \prod_{i=1}^{n-j+1} W^B_{\Omega(t^n-i)} W h^B_{\Omega(t^n-j-2)} \right) + W h^B_{\Omega(t^n-1)} \right] \]

\[ + \left( \sum_{j=2}^{n} \prod_{i=1}^{n-j+1} W^B_{\Omega(t^n-i)} + I \right) h_0, \tag{29} \]

where $z^{*n} = z_{t^n} = z_{t^n-n}$, if $(I - \prod_{i=1}^{n} W^B_{\Omega(t^n-i)})$ is invertible, i.e.

\[ \det \left( I - \prod_{i=1}^{n} W^B_{\Omega(t^n-i)} \right) = \prod_{i=1}^{n} W^B_{\Omega(t^n-i)} (1) \neq 0, \]

which implies $W^{t^n}_{\Omega^n} := \prod_{i=1}^{n} W^B_{\Omega(t^n-i)}$ has no eigenvalue equal to 1. As for simple fixed points, non-invertibility of the matrix in (29) implies there are directions of marginal stability in the dendPLRNN’s state space, along which we will find continuous sets of $n$-cycles, or the system is undergoing a bifurcation. Thus, we are approaching such a situation as one of the eigenvalues of $W^{t^n}_{\Omega^n}$ moves toward 1 and the matrix in (29) may become ill-conditioned.

Remark 1. These results about fixed points and $n$-cycles also hold for the mean-centred dendPLRNN. This can easily be seen by defining $W^{B}_{\Omega(t-1)} := A + W D^B_{\Omega(t-1)} M$ and noting that the elements of $D^B_{\Omega(t-1)}$ are now determined by the mean-centred latent states. That is $d^B_{m,t-1} = 1$ if $z_{m,t-1} > h_{m,b}$ and 0 otherwise. The rest of the calculations then proceed as above.

6.4.2. Sub-regions and discontinuity boundaries corresponding to system Eq. 24

Consider system Eq. 24 without external input and noise terms. Denoting $h_b = (h_{1,b}, h_{2,b}, \cdots, h_{M,b})^T$ in Eq. 24, for $b = 1, 2, \cdots, B$, we can order the elements $h_{j,1}, h_{j,2}, \cdots, h_{j,B}$ for every $j \in \{1, 2, \cdots, M\}$. Without loss of generality, let

\[ h_{j,1} < h_{j,2} < \cdots < h_{j,B}, \quad j = 1, 2, \cdots, M. \tag{30} \]
Then, for every \( j \), we define the intervals \( I_{j,b} \) as follows:

\[
I_{j,1} := (-\infty, h_{j,1}],
I_{j,b} := (h_{j,b-1}, h_{j,b}], \quad b = 2, 3, \ldots, B,
I_{j,B+1} := (h_{j,B}, +\infty).
\]

(31)

By definition of \( D_{\Omega(t-1)}^{(i)} \) in Eq. 24, the phase space is separated into \((B+1)^M\) sub-regions by \( MB(B+1)^{M-1}\) hypersurfaces as discontinuity boundaries. Every sub-region can be defined by the thresholds \( T \) as Cartesian product of suitable intervals in Eq. 31 for \( j \in \{1, 2, \ldots, M\} \). (Note that if in Eq. 30 we had “\( \leq \)” instead of strict inequalities “\(<\)”, obviously the number of intervals, hence sub-regions, would decrease.) In each sub-region the matrices \( D_{\Omega(t-1)}^{(b)} \), \( b = 1, 2, \ldots, B \), have a different configuration. Therefore, in Eq. 26 there are \((B+1)^M\) different forms for \( D_{\Omega(t-1)}^{B} \), and so for \( W_{\Omega(t-1)}^{B} \) and \( h_{\Omega(t-1)}^{B} \) as well. Hence, indexing \( D_{\Omega(t-1)}^{B} \), \( W_{\Omega(t-1)}^{B} \) and \( h_{\Omega(t-1)}^{B} \) as \( D_{r}^{B}, W_{r}^{B} \) and \( h_{r}^{B} \) for \( r \in \{1, 2, \ldots, (B+1)^M\} \), Eq. 24 can be written as

\[
z_{t} = W_{r}^{B} z_{t-1} + W h_{r}^{B} + h_{0}.
\]

(32)

To visualize the sub-regions and their borders, let for example \( M = 2 \) and \( B = 2 \). In this case there are 9 sub-regions divided by 12 borders. As illustrated in Fig. 6.4.2, there are different matrices \( D_{\Omega(t-1)}^{(b)} \), \( b = 1, 2 \), and \( D_{r}^{B} = D_{r}^{2} \), \( r = 1, 2, \ldots, 9 \), for each sub-region.

Figure S6. Example of different sub-regions and related matrices \( D_{\Omega(t-1)}^{(b)} \), \( b = 1, 2 \), and \( D_{r}^{B} = D_{r}^{2} \), \( r = 1, 2, \ldots, 9 \), for \( M = 2 \) and \( B = 2 \). Here, it is assumed that the components of \( h_{1} = (h_{1,1}, h_{2,1})^{T} \) and \( h_{2} = (h_{1,2}, h_{2,2})^{T} \) satisfy Eq. 30 with “\( \leq \)”.

6.4.3. Bounded orbits are compatible with the manifold attractor regularization

**Proposition 2.** The results of Theorem 2 are also true when the manifold-attractor regularization, Eq. 6, is strictly enforced for the dendPLRNN, Eq. 10.

**Proof.** Assume \( A, W, \tilde{\phi}(z_{t-1}) \) (see proof of Theorem 2 in Appx. 6.4.6 for the definition) and \( h_{0} \) have the partitioned forms

\[
A = \begin{pmatrix} I_{reg} & O^{T} \\ O & A_{nreg} \end{pmatrix}, \quad W = \begin{pmatrix} O_{reg} & O^{T} \\ S & W_{nreg} \end{pmatrix},
\]
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\[ h_0 = \begin{pmatrix} h_0^{\text{reg}} \\ h_0^{\text{nreg}} \end{pmatrix}, \quad \hat{\phi}(z_{t-1}) = \begin{pmatrix} \hat{\phi}_\text{reg}(z_{t-1}) \\ \hat{\phi}_\text{nreg}(z_{t-1}) \end{pmatrix}, \quad \text{(33)} \]

where \( I_{M_{\text{reg}} \times M_{\text{reg}}} =: I_{\text{reg}} \in \mathbb{R}^{M_{\text{reg}} \times M_{\text{reg}}}, O_{M_{\text{reg}} \times M_{\text{reg}}} =: O_{\text{reg}} \in \mathbb{R}^{M_{\text{reg}} \times M_{\text{reg}}}, O, S \in \mathbb{R}^{(M-M_{\text{reg}}) \times M_{\text{reg}}}, \) the sub-matrices \( A\{M_{\text{reg}}+1:M,M_{\text{reg}}+1:M\} =: A_{\text{reg}} \in \mathbb{R}^{(M-M_{\text{reg}}) \times (M-M_{\text{reg}})} \) and \( W\{M_{\text{reg}}+1:M,M_{\text{reg}}+1:M\} =: W_{\text{reg}} \in \mathbb{R}^{(M-M_{\text{reg}}) \times (M-M_{\text{reg}})} \) are diagonal and off-diagonal respectively. Furthermore, \( h_0^{\text{reg}}, \hat{\phi}_\text{reg}(z_{t-1}) \in \mathbb{R}^{M_{\text{reg}}} \) and \( h_0^{\text{nreg}}, \hat{\phi}_\text{nreg}(z_{t-1}) \in \mathbb{R}^{M-M_{\text{reg}}}. \)

In this case \( \|A\| = \sigma_{\text{max}}(A) = \max\{1, \sigma_{\text{max}}(A_{\text{reg}})\} \) and

\[
\left\| A^j W \hat{\phi}(z_{T-1-j}) \right\| = \left\| \begin{pmatrix} O \\ A_{\text{neg}}^j S \hat{\phi}_\text{nreg}(z_{t-1}) + A_{\text{neg}}^j W_{\text{neg}} \hat{\phi}_\text{nreg}(z_{t-1}) \end{pmatrix} \right\| \\
= \|A_{\text{neg}}^j S \hat{\phi}_\text{nreg}(z_{t-1}) + A_{\text{neg}}^j W_{\text{neg}} \hat{\phi}_\text{nreg}(z_{t-1})\|,
\]

\[
\left\| A^j W h_0 \right\| = \left\| \begin{pmatrix} O \\ A_{\text{neg}}^j S h_0^{\text{nreg}} + A_{\text{neg}}^j W_{\text{neg}} h_0^{\text{nreg}} \end{pmatrix} \right\| \\
= \|A_{\text{neg}}^j S h_0^{\text{nreg}} + A_{\text{neg}}^j W_{\text{neg}} h_0^{\text{nreg}}\|. \quad \text{(34)}
\]

Thus, for \( \sigma_{\text{max}}(A_{\text{reg}}) < 1 \)

\[
\|z_T\| \leq \|A\|^{T-1} \|z_1\| + \sum_{j=0}^{T-2} \left\| A^j W \hat{\phi}(z_{T-1-j}) \right\| + \sum_{j=0}^{T-2} \|A^j h_0\| \\
\leq \|z_1\| + (\hat{c} + \|h_0\|) \left( \|S\| + \|W_{\text{neg}}\| \right) \sum_{j=0}^{T-2} \|A_{\text{neg}}\|^j
\]

\[
= \frac{(\hat{c} + \|h_0\|) \left( \|S\| + \|W_{\text{neg}}\| \right)}{1 - \|A_{\text{neg}}\|} < \infty. \quad \text{(35)}
\]

6.4.4. Proof of Proposition 1

**Proof.** For \( A = (a_{ij}) \in \mathbb{R}^{M \times M}, \ W = (w_{ij}) \in \mathbb{R}^{M \times M}, \ e_t = (e_{1,t}, e_{2,t}, \ldots, e_{M,t})^T, \ s_t = (s_{1,t}, s_{2,t}, \ldots, s_{M,t})^T \) and \( C = (c_{ij}) \in \mathbb{R}^{M \times M}, \) writing Eq. 24 in scalar form yields

\[
z_{l,t} = \sum_{j=1}^{M} a_{ij} z_{j,t-1} + \sum_{j=1}^{M} w_{ij} \sum_{b=1}^{B} \alpha_b d_{j,t-1}^{(b)}[z_{j,t-1} - h_{j,b}] + h_{l,0} + \sum_{j=1}^{M} c_{lj} s_{j,t} + e_{l,t}
\]

\[
= \sum_{j=1}^{M} \left( a_{ij} z_{j,t-1} + w_{ij} \sum_{b=1}^{B} \alpha_b d_{j,t-1}^{(b)}[z_{j,t-1} - h_{j,b}] \right) + h_{l,0} + \sum_{j=1}^{M} c_{lj} s_{j,t} + e_{l,t}
\]

\[
=: \sum_{j=1}^{M} f_{l,j}(z_{j,t-1}) + h_{l,0} + \sum_{j=1}^{M} c_{lj} s_{j,t} + e_{l,t} =: F_l(z_{t-1}), \quad l = 1, 2, \ldots, M. \quad \text{(36)}
\]
We show that every $F_l$ is continuous and so Eq. 24 is a continuous PWL map. For this purpose, by Eq. 36, it suffices to prove that every $f_{l,j} (z_{j,t-1})$ is continuous. According to the definition of the intervals $I_{j,b}$, Eq. 31, for any $j \in \{1,2,\ldots,M\}$ we have

$$z_{j,t-1} \in I_{j,1} \Rightarrow d_{j,t-1}^{(b)} = 0 \quad \forall b = 1,2,\ldots,B,$$

$$z_{j,t-1} \in I_{j,s} \Rightarrow \begin{cases} d_{j,t-1}^{(b)} = 1, & b = 1,2,\ldots,s-1 \\ d_{j,t-1}^{(b)} = 0, & b = s,s+1,\ldots,B \\ s = 2,3,\ldots,B, \end{cases}$$

$$z_{j,t-1} \in I_{j,B+1} \Rightarrow d_{j,t-1}^{(b)} = 1 \quad \forall b = 1,2,\ldots,B.$$

Hence, for $l,j = 1,2,\ldots,M$, each function $f_{l,j} (z_{j,t-1})$ can be stated as

$$f_{l,j} (z_{j,t-1}) = \begin{cases} f_{l,j}^{(1)} = a_{lj} z_{j,t-1}; & z_{j,t-1} \in I_{j,1} \\ f_{l,j}^{(2)} = (a_{lj} + \alpha_1 w_{lj}) z_{j,t-1} - \alpha_1 w_{lj} h_{j,1}; & z_{j,t-1} \in I_{j,2} \\ \vdots \\ f_{l,j}^{(B)} = (a_{lj} + w_{lj} \sum_{b=1}^{B-1} \alpha_b) z_{j,t-1} - w_{lj} \sum_{b=1}^{B-1} \alpha_b h_{j,b}; & z_{j,t-1} \in I_{j,B} \\ f_{l,j}^{(B+1)} = (a_{lj} + w_{lj} \sum_{i=1}^{B} \alpha_b) z_{j,t-1} - w_{lj} \sum_{b=1}^{B} \alpha_b h_{j,b}; & z_{j,t-1} \in I_{j,B+1} \end{cases}$$

Since for every $b = 1,2,\ldots,B$,

$$\lim_{z_{j,t-1} \rightarrow h_{j,b}} f_{l,j}^{(b)} (z_{j,t-1}) = \lim_{z_{j,t-1} \rightarrow h_{j,b}} f_{l,j}^{(B+1)} (z_{j,t-1}) = f_{l,j}^{(b)} (h_{j,b}),$$

each function $f_{l,j} (z_{j,t-1})$ is continuous. Hence, Eq. 24 is a continuous PWL map in $z$ (but has discontinuities in its Jacobian matrix across the borders). Because of these properties, all the results established for standard PLRNNs in (Monfared & Durstewitz, 2020a;b; Schmidt et al., 2021) apply to the dendPLRNN as well, only that the sub-regions and discontinuity boundaries are different.

6.4.5. PROOF OF PROPOSITION 1

Proof. Defining $\tilde{z}_t$ as $B$ identical copies of $z_t$, 

$$\tilde{z}_t = \left( \begin{array}{c} \tilde{z}_{1,t} \\ \tilde{z}_{2,t} \\ \vdots \\ \tilde{z}_{M,t} \\ \tilde{z}_{M+1,t} \\ \vdots \\ \tilde{z}_{BM,t} \end{array} \right) := \left( \begin{array}{c} z_t \\ \vdots \\ z_t \end{array} \right)_{BM \times 1}$$

Using this, we can write Eq. 24 in the vector form

$$z_t = (F_1 (z_{t-1}), F_2 (z_{t-1}), \ldots, F_M (z_{t-1}))^T.$$
and likewise

\[
\hat{h} = \begin{pmatrix}
\hat{h}_1 \\
\hat{h}_2 \\
\vdots \\
\hat{h}_M \\
\hat{h}_{M+1} \\
\vdots \\
\hat{h}_{BM}
\end{pmatrix}
= \begin{pmatrix}
\hat{h}_1 \\
\hat{h}_2 \\
\vdots \\
\hat{h}_B
\end{pmatrix}_{BM \times 1}
\]

\[
\hat{h}_0 = \begin{pmatrix}
\hat{h}_{0,1} \\
\hat{h}_{0,2} \\
\vdots \\
\hat{h}_{0,M} \\
\hat{h}_{0,M+1} \\
\vdots \\
\hat{h}_{0,BM}
\end{pmatrix}
= \begin{pmatrix}
h_0 \\
h_0 \\
\vdots \\
h_0
\end{pmatrix}_{BM \times 1}
\]

\[
\hat{A}_{BM \times BM} = \text{diag}(A_{M \times M}, A_{M \times M}, \ldots, A_{M \times M}),
\]

\[
\hat{W}_{BM \times BM} = \begin{pmatrix}
\alpha_1 W_{M \times M} & \alpha_2 W_{M \times M} & \cdots & \alpha_B W_{M \times M} \\
\alpha_1 W_{M \times M} & \alpha_2 W_{M \times M} & \cdots & \alpha_B W_{M \times M} \\
\vdots & \vdots & \ddots & \vdots \\
\alpha_1 W_{M \times M} & \alpha_2 W_{M \times M} & \cdots & \alpha_B W_{M \times M}
\end{pmatrix},
\]

\[
\hat{C}_t = \begin{pmatrix}
\hat{c}_{s_{1,t}} \\
\hat{c}_{s_{2,t}} \\
\vdots \\
\hat{c}_{s_{M,t}} \\
\hat{c}_{s_{M+1,t}} \\
\vdots \\
\hat{c}_{s_{BM,t}}
\end{pmatrix} = \begin{pmatrix}
C_{s_1} \\
C_{s_2} \\
\vdots \\
C_{s_M}
\end{pmatrix}_{BM \times 1}
\]

\[
\hat{\epsilon}_t = \begin{pmatrix}
\hat{\epsilon}_{1,t} \\
\hat{\epsilon}_{2,t} \\
\vdots \\
\hat{\epsilon}_{M,t} \\
\hat{\epsilon}_{M+1,t} \\
\vdots \\
\hat{\epsilon}_{BM,t}
\end{pmatrix} = \begin{pmatrix}
\epsilon_t \\
\epsilon_t \\
\vdots \\
\epsilon_t
\end{pmatrix}_{BM \times 1}
\]

one can rewrite the dendPLRNN from Eq. 22 as

\[
\hat{z}_t = \hat{A}\hat{z}_{t-1} + \hat{W} \max(0, \hat{z}_{t-1} - \hat{h}) + \hat{h}_0 + \hat{C}_t + \hat{\epsilon}_t.
\]

Now performing the substitution

\[
\forall t \quad \hat{z}_t \leftarrow \hat{z}_t - \hat{h},
\]

Eq. 43 can be rewritten as the \( M \times B \)-dimensional “conventional” PLRNN Eq. 5 with

\[
\hat{h}_0 = (\hat{A} - I)\hat{h} + \hat{h}_0.
\]

6.4.6. Proof of Theorem 2

Proof. It can easily be shown that for every \( i \in \{1, 2, \ldots, M\} \)

\[
\alpha_b \left[ \max(\max(0, z_{i,t-1} - h_{i,b}) - \max(0, z_{i,t-1}) \right] \in \begin{cases}
[-\alpha_b h_{i,b}, 0] & \text{if } \text{sgn} (\alpha_b) = \text{sgn} (h_{i,b}) \\
[0, \alpha_b h_{i,b}] & \text{else}
\end{cases}.
\]

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By defining
\[ B \alpha \beta = \max(0, z_{t-1} - \max(0, z_{t-1})) = (\tilde{\phi}(z_{t-1}), \ldots, \tilde{\phi}_M(z_{t-1}))^T, \]  
\[ (47) \]

and
\[ c_{i,b}^{up} = \begin{cases} 0 & \text{if } \text{sgn}(\alpha \beta) = \text{sgn}(h_{i,b}) \\ \alpha \beta h_{i,b} & \text{else} \end{cases}, \quad c_{i,b}^{low} = \begin{cases} -\alpha \beta h_{i,b} & \text{if } \text{sgn}(\alpha \beta) = \text{sgn}(h_{i,b}) \\ 0 & \text{else} \end{cases}, \]
\[ (48) \]

we can conclude that
\[ c_{low} \leq \tilde{\phi}(z_{t-1}) \leq c_{up}, \]
where \( c_{low/up} = \sum_{b=1}^B c_{i,b}^{low/up} \). For \( c_i = \max\{|c_i^{low}|, |c_i^{up}|\} \) we have
\[ \tilde{\phi}(z_{t-1})^2 \leq c_i^2, \]
and so letting \( c = \max\{c_1, c_2, \ldots, c_M\} \) yields
\[ \left\| \tilde{\phi}(z_{t-1}) \right\| = \sqrt{\sum_{i=1}^M (\tilde{\phi}_i(z_{t-1}))^2} \leq \sqrt{\sum_{i=1}^M c_i^2} := \tilde{c}. \]  
\[ (49) \]

Since
\[ z_t = A z_{t-1} + W \tilde{\phi}(z_{t-1}) + h_0, \]
\[ (50) \]

for \( T \in \mathbb{N} \) and \( t = 2, \ldots, T \), computing \( z_2, z_3, \ldots, z_T \) recursively leads to
\[ z_2 = A z_1 + W \tilde{\phi}(z_1) + h_0 \]
\[ z_3 = A^2 z_1 + A W \tilde{\phi}(z_1) + W \tilde{\phi}(z_2) + [A + I] h_0 \]
\[ \vdots \]
\[ z_T = A^{T-1} z_1 + \sum_{j=0}^{T-2} A^j W \tilde{\phi}(z_{T-1-j}) + \sum_{j=0}^{T-2} A^j h_0. \]  
\[ (51) \]

Therefore, by Eq. 49, for every \( T \geq 2 \), we have
\[ \|z_T\| \leq \|A\|^{T-1} \|z_1\| + \tilde{c} \left\| W \sum_{j=0}^{T-2} \|A\|^j + \sum_{j=0}^{T-2} \|A\|^j \|h_0\| \right\|. \]  
\[ (52) \]

If \( \sigma_{\max}(A) < 1 \), then \( \lim_{T \to \infty} \|A\|^{T-1} = 0 \) and
\[ \lim_{T \to \infty} \|z_T\| \leq \tilde{c} \left\| W \sum_{j=0}^{\infty} \|A\|^j + \sum_{j=0}^{\infty} \|A\|^j \|h_0\| \right\| = \frac{\tilde{c} \left\| W \right\| \|h_0\|}{1 - ||A||} < \infty. \]  
\[ (53) \]