Gold Nanoparticles Based Optical Biosensors for Cancer Biomarker Proteins: A Review of the Current Practices

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Cancer prognosis depends on the early detection of the disease. Gold nanoparticles (AuNPs) have attracted much importance in biomedical research due to their distinctive optical properties. The AuNPs are easy to fabricate, biocompatible, surface controlled, stable, and have surface plasmonic properties. The AuNPs based optical biosensors can intensely improve the sensitivity, specificity, resolution, penetration depth, contrast, and speed of these devices. The key optical features of the AuNPs based biosensors include localized surface plasmon resonance (LSPR), SERS, and luminescence. AuNPs based biomarkers have the potential to sense the protein biomarkers at a low detection level. In this review, the fabrication techniques of the AuNPs have been reviewed. The optical biosensors based on LSPR, SERS, and luminescence are also evaluated. The application of these biosensors for cancer protein detection is discussed. Distinct examples of cancer research that have a substantial impact on both scientific and clinical research are presented.

Keywords: gold nanoparticles, LSPR, SERS, optical biosensor, protein biomarker, plasmonic resonance

1 INTRODUCTION

The biological molecule that is present in blood or any body fluids or tissues and is an indicator of either normal or abnormal condition in the body is defined as a biomarker by the National Cancer Institute. Recently, biomarkers have achieved a lot of importance in the early diagnosis of cancer (Christofi et al., 2019). Cancer is a very serious disease that can lead to the death of a person if untreated (Yang et al., 2018). Survival can be made possible with the early diagnosis of the condition. It has been seen that in the case of early diagnosis of cancer, the therapy is given to have more effective and the recovery rate is much higher in such cases as compared to late diagnosed cases (Hawkes, 2019). The prognosis of cancer also depends upon the examination of the primary tumor and on the detection of disseminated cancer cells in case of a malignant tumor (Haber and Velculescu, 2014). Tissue biopsy is most commonly used for the clinical diagnosis of cancers, but it is very costly, time-consuming, invasive, unsuitable for repeated testing, and also unavailable in some cancers like lung cancer (Cui et al., 2018).

Liquid biopsy is a type of biopsy in which the analysis of biomarkers is done in the non-solid biological tissue such as blood. This method is quite effective and advanced and encircles a large number of diseases and cancer. Thus, this technique has many advantages over conventional ones (Alimirzaie et al., 2019). It is inexpensive, non-invasive, feasible for repeated testing, and available to...
a large population without any advanced requirements. It also allows disease monitoring, its stage, and real-time effectiveness of treatment as well (El Rassy et al., 2018; Rojalin et al., 2020). The circulating biomarkers like tumor cells, nucleic acids, vesicles, and proteins are all analytes that are analyzed in the liquid biopsy (Li et al., 2017; Lane et al., 2018; Chang et al., 2019).

In proteomics, some protein biomarkers have been investigated in blood for cancer diagnosis (Lewis et al., 2018). Elevated levels of proteins have been recorded in cancer patients which are co-related with the metastasis, prognosis, and treatment of the disease. Prostate-specific antigen (PSA) is one of the common protein biomarkers assessed in the clinical identification of prostate cancer (Tkac et al., 2019). Similarly, cancer antigen 125 (CA 125) level is checked for ovarian cancer (Romeo and Seropian, 2021), alpha-fetoprotein (AFP) level is checked for liver cancer (Zhang et al., 2018), CA19.9 level is checked for gastric/pancreatic cancer (Subki et al., 2021), carcinoembryonic antigen (CEA) level is checked for colorectal cancer (Zhao et al., 2018), and cancer antigen 15.3 (CA15.3)/CA27.29 level is checked for breast cancer (Li et al., 2018). Sometimes autoantibodies are also produced by the immune system in cancer patients. These autoantibodies are also used as biomarkers for some types of cancers as well. These autoantibodies most commonly include immunoglobulin G (IgG) and immunoglobulin E (IgE). IgG and IgE levels are usually high in cancerous patients as compared to normal persons (Zang et al., 2019). ELISA, western blotting, mass spectrometry, and radioimmunoassay (RIA) are some of the most often used techniques for protein biomarker analysis. These classical approaches, on the other contrary, are insensitive, time-consuming, or difficult to implement. Picomolar LOD values are typical among the commercially available immunoassays. However, the protein biomarker concentrations in the blood associated with various types of cancer show a range of $10^{-16}$–$10^{-12}$ M in the blood. The low quantity of a given biomarker makes ELISA an ideal method for the detection of cancer proteins. There are a lot of cases where the biomarker is detected at an early stage of malignancy. But its application in hospital setting and as non-portable devices is not an ideal choice. As a result, it is imperative to create assays that are both sensitive and specific, as well as simple to use, for protein biomarker-based cancer diagnosis (Bakirhan et al., 2018).

In every aspect of daily science, nanotechnology has started new opportunities. Nanotechnology’s biological applications are progressing at a rapid pace to improve human health. The theragnostic platform for cancer detection is provided by nanocarriers (Ahmadian et al., 2019). Nanocarriers are one of a kind in terms of chemical solubilization, encapsulation, and disease marker detection capabilities. Among the numerous nanocarriers produced, gold nanoparticles (AuNPs) have garnered current scientific interest. Drug administration, tumor sensing, photothermal agents, and high-sensitivity biomarker testing are only a few of the uses of AuNPs (Medici et al., 2021). Other benefits of AuNPs are their simplicity of production, chemical stability, and biocompatibility.

This review focuses mainly on the surface plasmon properties of AuNPs for cancer treatment. The synthesis of AuNPs and important clinical biomarkers will be reviewed. The important physicochemical and optical properties of AuNPs and the techniques employed for cancer diagnosis will be discussed. The various strategies for detecting cancer protein biomarkers will be discussed in terms of their clinical application.

## 2 SYNTHESIS OF AUNPS

AuNPs can be synthesized using “Top-Down” and “Bottom-Up” strategies, which are two distinct methods (Man et al., 2018; Wahab et al., 2018; Zhu et al., 2020). Starting with bulk material and breaking it down into nanoparticles using various ways is the top-down strategy to synthesize AuNP. The bottom-up strategy, on the other hand, begins with the atomic level and works its way up to the nanoparticle level. Top-down synthesis methods include laser ablation, ion sputtering, UV and IR irradiation, and aerosol technology, whereas bottom-up approaches include reducing Au$^{3+}$ to Au$^{0}$. The methods to synthesize the AuNPs can be classified as in Figure 1.

### 2.1 Chemical Synthesis of AuNPs

#### 2.1.1 Turkevich Method of Synthesis of AuNPs

Turkevich (1951) proposed the use of aqueous citrate solutions to reduce gold (III) compounds, such as HAuCl₄, to produce AuNPs (Figure 2). The author’s experiments showed that the percentage of reducing to stabilizing agents has a significant impact on the size of the resulting nanoparticles (Polte et al., 2010). To produce AuNPs with many different shapes and sizes, borohydride was combined with chloroauric acid, which is a metallic salt of chloroaucric acid. The varying amounts of the metal salt nanowires, nanorods, triangular and spherical type AuNPs were obtained (Grzelczak et al., 2008). It is also feasible to produce anisotropic metallic nanoparticles using an aqueous surfactant-based colloidal chemical approach in the presence...
of ascorbic acid and CTAB (Sau and Murphy, 2004). The AuNPs synthesis has been extensively done by using the classical Turkevich method. The synthesis of spherical particles between 10 and 30 nm has been carried out by this relatively reproducible and simple technique (Dobrowolska et al., 2015; Schulz et al., 2014).

2.1.2 Polymer-Mediated Synthesis of AuNPs
In 1718, Helcher published a complete scientific article on polymer stabilized colloidal gold. According to numerous studies, metallic AuNPs and polymers have a considerable impact on particle size, stability, and distribution (Shenhar et al., 2005). Xinjiao et al., described a nanogold-based system successfully reduced to AuNPs by citrate and was encapsulated within the 154-block copolymer of polystyrene and poly (acrylic acid) (Figure 2). Such systems provide safe and effective diagnosis and targeted cancer treatment (Wang et al., 2008). Different polymers used in the synthesis of AuNPs include poly (ethylene glycol) (PEG) (Wang et al., 2020), Poly (N-vinylpyrrolidone) (PVP) (Fazleeva et al., 2021), chitosan (CS) (Hu et al., 2018), polystyrene (PS) (Gálvez-Vergara et al., 2020), poly (methyl methacrylate) (PMMA) (Wang and Seidel, 2021) and polyvinyl alcohol (PVA) (Amourizi et al., 2020).

2.1.3 The Brust Method
Methods for synthesizing AuNPs employing organic solvents, have been documented since 1994. It produces AuNP within the size range of 1.5–5.2 nm. This method uses tetraoctylammonium bromide (TOAB) as a phase transfer (Figure 2) to transfer gold salt from aqueous solution to organic solvent (e.g., toluene) (Salabat and Mirhoseini, 2018). Sodium borohydride and an alkanethiol are then used to decrease the gold to a more reasonable size. The alkanethiol brings the stabilization of AuNPs. This process causes the color to change from orange to brown (Mahato et al., 2019), (Tianimoghadam and Salabat, 2018).

2.1.4 Seed-Mediated Growth
It is possible to formulate the AuNP in a variety of geometries and shapes such as rods and stars. Seed-mediated growth is the most

**FIGURE 2** | Turkevich method, Burst method and polymer capped synthesis of AuNPs.
2.2 Physical Methods for Synthesis of AuNPs

2.2.1 UV-Induced Photochemical Synthesis of AuNPs

Shengchun Yang et al. used photochemistry to successfully synthesize colloidal gold with a controlled size of nanoparticles (Zhou et al., 1999). AuNPs can be synthesized by employing the function of steric hindrance (Figure 4). The steric hindrance can be achieved by the capping effect of polymers, dendrimers, or surfactants as soft templates that prevent the formation of aggregates. The UV radiation source of various wavelengths, like Transilluminator 48 W light, and participation of surfactant/polymer reagents will have a specific impact on particle dimensions, which implies that raising the polymerization degree decreases particle size (Sau et al., 2001).

In a study, Heparin functionalized colloids were generated using UV black-light lamp irradiation at approximately $\lambda = 366$ nm, and SERS (Surface Expanded Raman Spectroscopy) was carried out (del Pilar Rodriguez-Torres et al., 2014).

2.2.2 Laser Ablation Synthesis of AuNPs

Recently, the reduction of gold (III) tetrachloroaurate metallic precursors by photo-induced effects of a 532 nm laser beam resulted in nanogold particles with diameters smaller than 5 nm. The gold is reduced to AuNPs in top-down strategy (Figure 4). Aqueous sodium dodecyl sulphate (SDS) solutions were used as a templating agent in this technique, and the scientists looked at the effects of SDS concentrations and laser fluences on the produced AuNPs (Mafuné et al., 2001). In cancer biomarker applications, a two-step laser-assisted ablation technique was used to create surface enhanced Raman scattering (SERS) The laser-activated nano-rods include the bridging of connective tissue gaps (Matteini et al., 2010).

2.3 Ultrasound-Assisted Synthesis of AuNPs

When AuNPs are subjected to ultrasonication, the gold ions are reduced and form AuNPs (Figure 4). The characteristics of the particles can be adjusted. In one investigation, an ultrasound wave generator (200 kHz frequency, 20–200 W power output)
was employed to maintain a consistent temperature for the ultrasonic-aided reduction of gold ions in a water bath while the presence of 2-propanol was also present. It was necessary to use a variety of stabilizers in the classic ultrasound-assisted synthesis process to assure repeatability and tunability. These included citrate, poly (N-vinyl-2-pyrrolidone), triphenylphosphine, disulfide, and several other dendrimers.

Colloidal gold synthesis using an ultrasonic field is an intriguing and upfront method that may be applied in chemical and biological synthesis methods (Jiang et al., 2004), (Okitsu et al., 2001).

2.4 Unconventional Green Biological Synthesis of AuNPs

Gold nanoparticles are typically prepared using chemical synthesis, which is a low-cost, high-volume process that yields reliable results (in terms of size and shape). However, the use of toxic solvents, contamination from precursor molecules, and deadly byproducts are some of the drawbacks to chemical synthesis (Shedbalkar et al., 2014). Modern nanotechnology research has turned its focus to biological synthesis to address these problems (Figure 4). Some of the biological sources are either found in nature or are revalued resources utilized during the creation of colloidal nanogold. These compounds include derivatives derived from plants, bacteria, fungi, algae, yeast, and viruses (Thakkar et al., 2010).

3 CHARACTERIZATION OF AUNPS

3.1 LSPR, Size, Color and Electric Field Enhancement

When the matter is exposed to light, numerous processes take place. Light may be absorbed. The scattering phenomenon occurs when light is dispersed. On the other hand, fluorescence occurs when light is re-emitted. Gold is a noble metal with many free electrons. When AuNPs are subjected to light, the electric field of the light causes the conduction-band electrons at the particle’s surface to collectively oscillate with respect to the ionic core of the nanoparticle (Huang et al., 2007). Concisely, the surface plasmon resonance is the coherent oscillation of metal-free electrons in resonance with the electromagnetic field (SPR). The SPR and LSPR are compared in Figure 5. The SPR equipment employed a monochromatic light source with a wide range of incident angles in the trials. As a result, the lowest point on the reflectivity vs. incident angle curve represents the plasmon excitation. It depicts that the coupling condition varies and the minimal peak shifts when the refractive index changes near the layer. For metal nanoparticles, the localized plasmons are excited by direct illumination, regardless of the illumination angle. The intensity of the transmitted light decreases because of the plasmon’s evanescent field surrounding the NP if the criterion on energy (the wavelength of the received light) is met. The abundance of readily polarized conduction electrons in AuNPs necessitates the use of nonlinear optical processes and electromagnetic fields as a preferred mode of interaction. LSPR has now been widely employed in AuNP based biosensors.

Michael Faraday was the first to make the connection between AuNPs’ optical properties and their minuscule size at the Royal Institute in London. In his 1852 presentation entitled “Experimental Relations of Gold (and Other Metals) to Light,” the plasmonic properties were described. Traditional surface plasmon resonance (SPR) has been now replaced with localized surface plasmon resonance (LSMR). SPR makes use of gold film, while LSPR utilizes AuNPs. LSPR generates a prominent resonance absorbance peak in the visible region of light’s spectrum. AuNPs scatter light with an increase in intensity and at the same or a shifted frequency (elastic scattering-Resonance Rayleigh scattering) when light contacts their surface (inelastic scattering-surface enhanced Raman scattering). The location of this peak is highly dependent on the particle’s local refractive index. Instead of the angle seen in the traditional SPR method, the LSPR equipment can detect small variations in the wavelength of the absorbance location. LSPR offers numerous benefits, including the fact that it does not require a prism to combine the light, has a relatively short
electromagnetic field decay duration, and is less susceptible to temperature drift. Sensor chips may be manufactured more cost-effectively (Focsan et al., 2017).

Gold nanoparticles absorb and scatter light with extraordinary efficiency. Their strong interaction with light occurs because the conduction electrons on the metal surface undergo a collective oscillation when they are excited by light at specific wavelengths (Cabuzu et al., 2015; Vines et al., 2019). In our study, the UV–visible spectra of the AuNPs samples were recorded for the wavelength range 200–800 nm at 2 min interval at 25°C on a Hewlett-Packard 8452A diode array spectrophotometer (Jiang et al., 2007). Gold nanoparticles represent specific wavelengths, emission frequencies, and emission wavelengths that are highly dependent on the size, shape, surface, and aggregation state of the nanoparticles (Kim and Lee, 2018). AuNPs with internal thiol groups on their metallic core were produced in a study. These demonstrated a UV-visible absorbance peak at 517 nm consistent with their surface plasmon resonance. These AuNP are not only soluble and stable in water, but also in different organic solvents such as dichloromethane or methanol (Ouellette et al., 2018). The characteristic optical properties and SPR of AuNP are summarized in Table 1.

The changes in the pH have a drastic effect on the SPR of AuNPs especially in the case of functionalized nanoparticles. Researchers found that by varying the pH of AuNPs, the APTES assembly was controlled on the AuNP surface. This allowed for the reversible assembly of AuNPs. To monitor the optical behavior of the reversible assembly as a function of pH, a UV–vis spectrometer was utilized. In solution, the color changed from blue to bluish, followed by purple to wine red as pH increased from 9.8 to 12.0. The optical properties of AuNP assemblies showed an opposite phenomenon as pH decreased from 12.0 to 9.8 and the solution color changed from wine red, purple, and bluish purple to bluish purple to wine red as pH increased (Liu et al., 2021). In metallic nanoparticles, LSPR causes resonances and enormous electric fields because of electric field resonance. Optical features of the structure have a greater effect on electric field enhancement than do material properties (Singh et al., 2013; Bensebaa, 2013). Yuan et al. prepared mercaptopypyridine-functionalized AuNPs for fiber-optic surface plasmon resonance Hg$^{2+}$ sensing. The basic principle was relied on the coordination between Hg$^{2+}$ and nitrogen in the pyridine moiety. The electrical field intensity enhanced six times over the pure sensing gold film structure with the addition of AuNPs (Yuan et al., 2019).

### 3.2 X-Ray Crystallography (XRD)

Crystal structure and cell parameters are studied in relation to nanoparticle size and shape using XRD spectroscopy, a technique that can characterize nano powders of any size and shape (Vorontsov and Tsybulya, 2018). Van-Dat et al., Doan reported the biosynthesis of AuNPs Using Litsea cubeba Fruit Extract. XRD patterns were used to identify the crystalline structures of the biosynthesizedAuNPs. There were distinct peaks in the XRD pattern ofAuNPs at 2 theta angles of 38.12°, 44.27°, 64.42°, and 77.47°, which corresponded to the hkl planes of (111), (200), (220), and (311) respectively, for the face-centered cubic structure of Au (Doan et al., 2020). Bimetallic silver/gold nanoparticles were synthesized via starch-mediated synthesis. The Ag/AuNPs and AuNPs XRD spectrum indicated the bulk face-centered cubic (FCC) Ag and Au XRD patterns. In both bulk FCC Ag and Au, the diffraction peaks detected at 2 theta were 38.3, 44.5°, 64.8°, 77.8°, and 81.8° that corresponded to crystallographic planes (111), (200), (220), and (311) and (222), respectively (Lomeli-Marroquin et al., 2019). Ehsan Koushki and co studied the effect of glucose and glucose oxidase on the UV–vis spectrum of AuNPs and reported the hkl planes of 111, 200, 220 and 311 in XRD spectrum (Koushki et al., 2020).

### 3.3 SERS and Electrical Field Enhancement

SERS is a surface-sensitive technique that works on amplified Raman scattering, when the molecules are adsorbed on rough metal surfaces or nanostructures (Bell et al., 2020). The electric field enhancement is the common mechanism involved in the SERS based metallic biosensors (Li et al., 2019). The surface plasmons are stimulated by the incident light. When the plasmon frequency, is in resonance with the radiation, the field enhancement is maximum (for spherical particles). The plasmon oscillations must be perpendicular to the surface for scattering to take place; if they are in plane with the surface, no

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**Table 1**: The characteristic optical properties of AuNPs.

| Shape             | Synthesis methodology | Size (nm) | Color     | SPR (nm)        | Ref                        |
|-------------------|-----------------------|-----------|-----------|-----------------|----------------------------|
| Spherical         | Laser ablation        | 17 and 32 | Dark pink | 536             | Tommaleh et al. (2020)     |
| Spherical         | Green synthesis       | between 20 and 50 | Ruby red | 537             | Vijaya Kumar et al. (2019) |
| Semi-spherical    | Turkevich method      | 10–13     | Purple    | 529             | Koushki et al. (2020)      |
| Spherical         | Polymer mediated      | <50       | Yellow to varying colors | 520 to 540 of different systems | Jawarka and Chatterjee, (2006) |
| Spherical         | Green synthesis       | 5–20      | Ruby red  | 526             | Khatua et al. (2020)       |
| Spherical         | Green synthesis       | 25.5      | Purple    | 530             | Folorunso et al. (2019)    |
| Nanospheres       | Green synthesis       | 28.4      | Red       | 532             | Lee et al. (2019)          |
| Nanospheres       | Green synthesis       | 190.7 (CS capped) | Red      | 537 (CS capped) |                             |
| Nanostars         | Growing nanorods from seeds | 97.8 | Blush     | 800             |                             |
| Nanorods          | Growing nanorods from seeds | 123.9 (CS capped) | Pink | 786 (CS capped) |                             |
| Nanorods          | Growing nanorods from seeds | 10   | Yellowish | 514 and 815 | Qamar et al. (2022)        |
scattering will take place (Palermo et al., 2021; Lu et al., 2020). The NP-derived nanostructured metal with SERS may deliver up to 3,000 times more enhancements in the electric field, which is equivalent to an increase in Raman scattering that is 14 orders of magnitude greater in magnitude. This improvement enables a single-molecule level of sensing. Jaijun Lu et al, investigated electric field-modulated SERS of metal-polymer hybrid. This technique improved the detection sensitivity (Lu et al., 2020). Zu-Yin Deng and co, synthesized gold and magnetic Fe2O3 nanoparticles that were sandwiched between layers of the biochip. Fe2O3 nanoparticles were used in the fabrication of single (Au/Fe2O3/Au) and multilayer (Au/Fe2O3/Au/Fe2O3/Au) chips to detect bovine serum albumin (BSA). The BSA antigen was detected with an SNR of 5.0 using a single-layer device. SERS was used to map the electromagnetic field enhancement. Using an external magnetic field, the single-layer chip containing Au nanoparticles was tested. In a field of 12.5 G, the strongest signal was detected. In a 62.5-G field, we found peaks caused by other carbon–hydrogen molecules (Deng et al., 2019). Due to its capacity to quench and multiplex fluorescence and its compatibility with short probe DNA sequences, SERS differs from conventional fluorescence-based techniques. Khalil et al., developed dual platform based on graphene oxide and AuNPs and a short DNA probe for SERS based DNA biosensing. The authors described a unique and PCR free SERS-based DNA detection technique for the identification of an endangered species, the Malayan box turtle (MBT), using dual platforms and short DNA probes (Cuora amboinensis). These two platforms were linked by covalently tying together graphene oxide-gold nanoparticles (GO-AuNPs) that were functionalized with capture probe 1 and AuNPs that were modified with capture probe 2 and a Raman dye (Cy3) via hybridization with the corresponding target sequences in order to detect them. Locally enhanced electromagnetic field “hot spots,” generated at junctions and interstitial fuses of nanostructures, enabled considerable amplification of SERS signals when the two platforms were coupled. As a result, the biosensors were able to reach a lower limit of detection (LOD) as low as 10 fm by employing two SERS active substrates and short-length probe DNA sequences. Even a single base mismatch in the target DNA could not fool the biosensor, which was also able to distinguish between six closely related non-target DNA sequences with high accuracy. That SERS biosensor was deemed fit to detect genespecific biomarkers for numerous disorders, including cancer (Khalil et al., 2019). Two-dimensional (2D) gold nanoparticles can possess novel physical and chemical properties, which will greatly expand the utility of gold nanoparticles in a wide variety of applications ranging from catalysis to biomedicine. Muhammad alamri and co, developed plasmonic AuNPs on 2D MoS2/Graphene Vander-Waals heterostructures for high-sensitivity SERS. In situ electron-beam evaporation of Au at temperatures between 300’ and 350’C in high vacuum resulted in the deposition of AuNPs on MoS2/graphene. As a SERS probe molecule, Rhodamine 6G (R6G) was shown to be five orders of magnitude more sensitive than AuNPs/graphene under the same excitation conditions, and this was done with a nonresonance 633 nm laser. Resonance 532 nm laser excitation resulted in a sensitivity increase from 5*10⁻⁸ M to 5*10⁻¹⁰ M. According to a density functional theory calculation, the observed increase in SERS sensitivity was attributed to the combination of the electromagnetic mechanism of plasmonic AuNPs with the chemical mechanism (Alamri et al., 2019).

4 FUNCTIONALIZATION WITH RECOGNITION ELEMENTS ON AUNPS (TRANSUDCERS)

The biosensors include both recognition elements and the transducer components, which work together to enable selective/specific binding with the target analytes to produce a signal. The AuNPs act as transducer and produce signal based on LSPR, SERS, chemiluminescence. Functionalization of NPs involves conjugation of molecules on the surface of the particles. The high surface to volume ratio allows efficient functionalization of particles to suit our needs (Thiruppathi et al., 2017). Table 2 includes some of the functional groups on the AuNPs. Farshchi and co., reported the polyethyleneimine-gold nanoparticles coupled to dye/metal ions electrochemical biosensor for the detection of three breast cancer biomarker proteins. Fe2O4 magnetic nanoparticles and cysteamine-functionalized AuNPs were used in the study to create a new electroconductive interface. In the electrochemical investigation of antibody-antigen binding, the constructed interface was used as a substrate for signal amplification. Anti-PSA antibody was bio-conjugated with Fe3O4 nanoparticles and drop-casted onto the surface of glassy carbon electrodes for this purpose (GCE). Secondary antibody (HRP-Ab2) encapsulated on AuNPs covered by cysteamine was fixed on the GCE modified electrode. Under ideal experimental circumstances, a detection limit of 0.001 μg.L⁻¹ of PSA was achieved (Farshchi et al., 2020). In another study, Mahani et al., reported. The anti-PSA antibody was covalently coupled to the AuNPs. The antibody–PSA combination was also supported by MD simulations. Antigen binding caused the dielectric medium to change its refractive index, resulting in a shift in the LSPR peak of the probe. Accurate detection limits (0.2 ng ml⁻¹) and calibration sensitivities of 43.75 nm/(ng mL⁻¹) were achieved (Mahani et al., 2021).

5 CLINICAL PROTEIN BIOMARKERS FOR EARLY CANCER DETECTION

Detection and treatment of cancer are strongly dependent on early diagnosis. Tissue biopsy and traditional diagnostic methods such as ELISA have several drawbacks, including failure to identify at an early stage and the need for complicated procedures. Another method for diagnosing the existence of cancer and monitoring its progression is to screen for tumors using proteins contained in bodily fluids such as plasma, urine, and cells/tissues. In normal cells, these indicator proteins are produced at healthy levels; but, in a cancer environment, their levels rise by several orders of magnitude (Misek and Kim, 2011; Surinova et al., 2011; Nolen and Lokshin,
calcium (Ca)-stimulated CT levels (Niederle et al., 2020). Thyroid nodules can reveal medullary thyroid cancer (MTC) formation (Kwaan and Lindholm, 2019). CT screening for development of the tumor by interfering with blood vessel IL-8 are upregulated in bladder cancer, posing a threat to the bladder cancer. In the case of bladder cancer, morphological indicators and clinical characteristics in genetic variants are associated with a wide range of high for bladder malignancy. Early detection of bladder cancer extremely malignant tumor. Recurrence and death rates are very to its high prevalence and aggressiveness, bladder cancer is an most common type of cancer. Protein indicators such as Alpha-

2012). ALK is a transmembrane tyrosine kinase receptor gene. During development, it is biologically expressed in the nervous system, but it vanishes after birth. Anaplastic large-cell lymphoma (ALCL) patients’ NPM1 fusion with ALK was first discovered in 1994. ALK has been linked to several malignancies, including non-small-cell lung cancer (NSCLC) (Du et al., 2018). The yolk sac and liver release the most alpha-fetoprotein (AFP), which is the most common blood protein in human embryos. In the mother’s blood, AFP levels peak between 28 and 32 weeks of pregnancy, decline rapidly after delivery and then spike again 8–12 months later. Adult AFP levels should not exceed 20 ng/ml. AFP is generated and secreted at a considerably higher rate in liver tumor cells (Shah et al., 2020). Among women, breast cancer is the most frequent invasive cancer and the second most common cause of cancer death after lung cancer. The clinical use of the cancer markers CA15-3, CA27-29, and Carcinoembryonic has been proven (EBSCOhost, 2021). Serum CEA, CA72-4, CA19-9, CA15-3, and CA12-5 are used to identify gastric cancer (Chen et al., 2017). KELIM, a reliable early indication of tumor chemosensitivity, was computed using CA-125 longitudinal kinetics over the first 100 treatment days in ovarian cancer (You et al., 2020). Similarly, a new ovarian cancer biomarker is transthyretin (TTR) and serum human epididymis protein 4 (HE4) (Zheng et al., 2018). In addition to its high prevalence and aggressiveness, bladder cancer is an extremely malignant tumor. Recurrence and death rates are very high for bladder malignancy. Early detection of bladder cancer and recurrences is essential to a long life expectancy. Several genetic variants are associated with a wide range of morphological indicators and clinical characteristics in bladder cancer. In the case of bladder cancer, fibrin/fibrinogen are important indicators. Thromboxin, IL-1, and IL-8 are upregulated in bladder cancer, posing a threat to the development of the tumor by interfering with blood vessel formation (Kwaan and Lindholm, 2019). CT screening for thyroid nodules can reveal medullary thyroid cancer (MTC) at an early stage by measuring both basal calcitonin (CT) and calcium (Ca)-stimulated CT levels (Niederle et al., 2020). Human IgG4-based Odrornexmab is a first-in-class, hinge-stabilized, human IgG4-based bsAb (antibody). It has demonstrated good safety and tolerability, as well as early efficacy in patients with relapsed/refractory (R/R) B-cell non-Hodgkin lymphoma (B-NHL) (Bannerji et al., 2020). In men between the ages of 15 and 35, germ cell tumors (GCTs) are the most common type of cancer. Protein indicators such as Alpha-

6 AUNPS BASED OPTICAL BIOSENSING OF CANCER PROTEINS

The sensing mechanisms of optical biosensors that utilize AuNPs for cancer diagnosis, are based on LSPR, SERS, and chemiluminescence. LSPR is an optical phenomenon that occurs when light photons interact with AuNP’s conduction band. It results in the collective oscillation of valence electrons and absorption in the ultraviolet-visible (UV-Vis) band. When a laser is used as the light source, the technique used is Raman spectroscopy. The SERS technique works by amplifying the Raman response of an analyte when it interacts with the surface plasmon of metals such as AuNPs. Luminescence is a broad term that refers to the emission of light that is not caused by a high temperature. Chemiluminescence is a light-emitting technology that is based on an exciting intermediate in a chemical reaction. When this intermediate reaches the ground state, it emits light. In contrast to fluorescence, electrons in chemiluminescences materials are activated via a chemical reaction rather than photon absorption. Surface plasmon resonance gives AuNPs adjustable optical characteristics (Figure 6).

6.1 Optical Biosensing Based on SPR/ LSPR-Enhanced Absorption

Colorimetric biosensing and Refractive index-based biosensing are the sensing mechanisms involved in LSPR devices. The small changes in refractive index are measured and the color changes are observed. The colorimetric analysis is a method that compares the color variations of a solution to determine the concentration of the analyte. There is no need for a fluorescent label in the case of a refractive index. For cancer protein biomarkers, AuNPs revealed a single LSPR shift as a signal reading. AuNPs are utilized to diagnose bladder cancer, according to Jazayeri and others. The antibody was detected using anti-survivin-coated AuNPs, and the findings were compared to ELISA. The AuNPs coupled with an anti-survivin antibody can detect bladder cancer in its early stages (Jazayeri et al., 2020). The citric acid reduction technique was used by Mahani et al. to make simple and cost-effective AuNP. These nanoparticles were able to identify prostate cancer in its early stages. The ultra-sensitive

| TABLE 2 | Functionalization of AuNPs. |
|----------------|-----------------------------|
| Nano system    | Functional group and ligand  | Targeted application                      | Ref               |
| AuNP           | PEG Aminolated and Thiolated CLPFFD peptide- H-N-terminated thiol-PEG ligands | Lateral Flow Detection of Bisphenol A Ihibit A(β)-fibrillation | Lin et al. (2018) |
| Hollow Au Nanospheres and Au Nanorods | Methionine linked to AuNPs via dithiocarbamate Amino acid (Methionine) | Inhibit A(β)-fibrillation | Ruff et al. (2018) |
| pH responsive DNA-AuNPs | DNA/MUC1 aptamer Aromatic aminoacid | Tumor imagini Tumor drug delivery and imaging | Gupta et al. (2021) |
| AuNPs          | Folate                      | Anticancer                                 | Sanchakov et al. (2021) |
|                |                             | Lipid corona                               | Chen et al. (2021) |
|                |                             |                                             | Maty et al. (2021) |
A label-free nano-biosensor was created to measure PSA in serum. It could detect PSA at low concentrations of 0.2 ng ml\(^{-1}\). Based on the hydrogen bonding between PSA and antibody, the LSPR method was utilized (Mahani et al., 2021). Retout et al. described the preparation of peptide-functionalized AuNP using a colorimetric LSPR-based fast and selective protein detection technique. At concentrations as low as 20 nM, the system proved effective, with signals appearing in less than 5 min (Retout et al., 2016). Kim and his colleagues created the refractive index sensor utilizing AuNP-based optical fibers. AuNPs are a kind of nanoparticle that attaches to the optic fiber and improves its stability. Thyroglobulin is an immunoglobulin that has been identified as a thyroid cancer biomarker with a LOD of 0.19 pg/ml. The data were examined to see if the biomarker might be detected in cancer patients’ sera (Kim et al., 2019). Figure 7 depicts the visual color changes in AuNP based LSPR for the detection of small biological molecules and cells.

### 6.2 Optical Biosensing Based on SERS

AuNPs can be used as protein biosensors employing surface-enhanced Raman spectroscopy (SERS), also known as surface-enhanced Raman scattering. As a surface-sensitive method, it has the potential to identify single molecules (Blanco-Formoso and Alvarez-Puebla, 2020). It utilizes molecules adsorbed on rough metal surfaces or nanostructures like plasmonic AuNPs. A molecule’s vibrational spectrum can be boosted by several orders of magnitude with this method (Moskovits, 2005). Direct and indirect methods of SERS sensing are the two main sensing mechanisms involved in these devices. In direct sensing, an analyte molecule is directly attached to a plasmonic substrate, and the vibrational modes of the analyte are reflected in the wavelengths of the resulting spectral characteristics. Rather than the analyte itself, the SERS signal is obtained using a reporter molecule (usually a dye or another significantly Raman scattering molecule. Due to the non-linearity of SERS enhancement at high analyte concentrations, the adsorption of molecules onto nanoparticle surfaces is not always uniform, and inefficient “hot spot” formation due to large particle spacing results in decreased enhancement. So, it can be difficult to correlate spectral intensity to concentration when direct sensing is used. Indirect sensing approaches can circumvent this drawback by selectively capturing analyte molecules and bringing them close to the augmenting surface using capture ligands, molecular recognition agents, or antibodies. However, because indirect sensing does not directly probe the molecule of interest, we are unable to learn about the molecule’s vibrational modes (Moore et al., 2018). SERS and hollow-core photonic crystal fiber (HCPCF) were employed by Dinish and others to detect protein biomarkers with exceptional sensitivity. For the nanoprobe, powerful Raman active molecules were attached to the surface of AuNPs, which can be used in conjunction with recognition element species to identify specific molecules. The biosensor was put to the test against MCF, a breast cancer cell line, and compared to an ELISA. In a sample volume of 10 nL, the nano-system was able to identify 100 pg of proteins (Dinish et al., 2012). Similarly, to explore the link between malignant exosomes and protein markers for cancer diagnosis, shin et al. used SERS principal component analysis (PCA). Cells from the PC9 and H1299 strains were used to investigate the effect. For this study, the researchers looked at the Raman peaks of four different exosomal protein identifiers: CD9, CD81, EpCAM, and EGFR (Shin et al., 2018). Biomarkers for lung and breast cancer treatment included elevated levels of IL-6 in the serum of patients. Inflammatory and cancer-promoting cytokine interleukin-6 (IL-6) was recently discovered by Muhammad et al., in a label-free, delicate, and selective biosensor. The IL-6...
various cancer cell lines. The system has the potential to detect the malignancy signals from probe device of AuNPs for cancer detection. The SERS based (Muhammad et al., 2021).

SERS-based aptamer biosensor has been demonstrated via electrogenerated chemiluminescence bioassay was developed α of clinical diagnostics (Zhang H. et al., 2020). For the detection sensitive, and reliable tool for the detection of exosomes in serum which depicts that the ECL biosensor is a viable, sensitive and precise detection of exosomes from human (OVCAR, HeLa, and HepG2 cells). It also facilitated the surface proteins obtained from different kinds of tumors sensing platform has high selectivity towards exosomes and 1,000 times lower than the conventional ELISA method. The ECL obtained from HeLa cell lines is 30 particles µL −1 which was activity of AuNPs-MXenes-Apt. The detection limit for exosomes increased surface area, exceptional conductivity, and catalytic detection of exosomes contributed to the synergistic effects of

6.3 Optical Biosensing Based on AuNP-Induced Luminescence

The Luminescence-based optical biosensors use either fluorescence or chemiluminescence for detection. It offers a wide range of advantages i.e., increased selectivity and flexibility. The colorimetric type fluorescence-based biosensors give visual results by using AuNP fluorescence or fluorescence resonance energy transfer (FRET) (Elahi et al., 2019), (Saeed et al., 2017). Zhang and others created ultrasensitive electrogenerated chemiluminescence (ECL) biosensor for exosomes and their surface proteins by forming AuNPs adorned Ti3C2 MXenes hybrids with aptamer modification in situ (AuNPs-MXenes-Apt). Exosomes were efficiently collected using this method using an exosome-recognized CD63 aptamer modified electrical interface. A highly sensitive ECL biosensor for the detection of exosomes contributed to the synergistic effects of increased surface area, exceptional conductivity, and catalytic activity of AuNPs-MXenes-Apt. The detection limit for exosomes obtained from HeLa cell lines is 30 particles µL -1 which was 1,000 times lower than the conventional ELISA method. The ECL sensing platform has high selectivity towards exosomes and surface proteins obtained from different kinds of tumors (OVCAR, HeLa, and HepG2 cells). It also facilitated the sensitive and precise detection of exosomes from human serum which depicts that the ECL biosensor is a viable, sensitive, and reliable tool for the detection of exosomes in clinical diagnostics (Zhang H. et al., 2020). For the detection of α-fetoprotein (AFP), a proximity hybridization-regulated electrogenerated chemiluminescence bioassay was developed via gold nanoparticles (AuNP) sensitization and target-induced quenching mechanism (Gao et al., 2017). The PLA-ECL bioassay was revealed to be more rapid, efficient selectivity, easy operation, precise accuracy, and wide detachable range, which are favorable for the detection of AFP in serum samples. The detachable limit for AFP was found to be 0.04 ng/ml. The bioassay can detect 300 a.m. (~9,000 copies) of prostate-specific antigen in buffer and 3 fM in 10% serum. Moreover, three protein cancer markers were detected at low pM concentration of buffer and 10% serum. Figure 9 demonstrates the application of AuNPs based on the principle of chemiluminescence.

7 CLINICAL APPLICATIONS OF CANCER PROTEINS BASED AUNP BIOMARKERS

AuNPs can improve conventional tests by improving sensor-analyte interactions. For cancer proteins, the detection limit (LOD) was increased by using AuNPs on ELISA plates (Ambrosi et al., 2010). UV-Vis spectroscopy may be used to determine the amounts of Au NPs in the presence and absence of proteins (Kuntamung et al., 2021). AuNPs-based bio-barcode assays were found to be even more sensitive than ELISA-based procedures without enzymatic amplification. Using immunomagnetic beads, magnetic separation can be utilized to isolate proteins from aqueous solutions. Immunomagnetic beads and AuNP conjugates are placed between the proteins. After the magnetic separation, the barcode oligonucleotides are rehybridized and then detected with an Au-NP catalyzed silver enhancement chip-based scano-metric assay. PSA may be rehybridized and then detected with an Au-NP catalyzed silver enhancement chip-based scano-metric assay. PSA may be

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![Figure 8](image-url) | AuNP based SERS for metastatic cancers diagnosis.
**TABLE 3 |** AuNPs-based optical biosensors as cancer protein biomarkers.

| Protein marker | Cancer type               | Optical techniques | Sensitivity lower limit/Linear range | References                           |
|----------------|--------------------------|--------------------|--------------------------------------|--------------------------------------|
| CEA            | Liver, ovarian, testicular | SERS               | 0.0001–100.0 ng ml\(^{-1}\)          | Medetallbyoglu et al. (2020)          |
| HER2           | Breast, gastric, esophageal | Chemiluminescence | -                                    | Zhang P. et al. (2020)               |
| SCC            | Esophageal, lung, ovarian | FDG-PET            | -                                    | Peng et al. (2020)                   |
| PSA            | Prostate cancer          | LSPR               | 100 fg/ml                            | Sanders et al. (2014)                |
| PSA            | Prostate cancer          | SERS               | 1 pg/ml                              | Grubisha et al. (2003)               |
| PSA            | Prostate cancer          | LSPR-Quenchers/ enhancers | 0.032 pg/ml                          | Liu et al. (2013)                    |
| AFP            | Liver, ovarian, testicular | LSPR               | 93.11 fg/ml                          | Kim et al. (2021)                    |
| CA19-9         | Bile duct, gastrointestinal | Luminescent       | 0.007 U ml\(^{-1}\)                 | Alartaj et al. (2018)                |
| CA72-4         | Bile duct, gastrointestinal | Chemiluminescence | -                                    | Hu et al. (2019)                     |
| Osteocalcin    | Bone                     | Luminescent        | -                                    | Matsuyama et al. (2018)              |
| CYFRA 21–1     | Lungs                    | Luminescent        | 0.08–500 ng/ml                       | He et al. (2013)                     |
| TPA            | Lungs                    | SERS               | -                                    | Hong and Li, (2013)                  |
| 5-HIAA         | Carcinoid                | SERS               | 1.2 ng/ml/12 min                     | Zhang Y. et al. (2020)               |
| NMP 22         | Bladder                  | Luminescent        | 0.05 pg ml\(^{-1}\)                 | Othman et al. (2020)                 |
| PSA            | Prostate                 | SERS               | 0.1 μg/L\(^{-1}\)                   | Oubibi et al. (2021)                 |
| S100           | Melanoma                 | SERS               | 0.0001 ng/ml                         | Song et al. (2022)                   |
| Thyroglobulin  | Thyroid                  | LSPR               | -                                    | Kim et al. (2021)                    |
| CA27.29        | Breast                   | SERS               | CA15-3 (0.99 U ml\(^{-1}\)), CA27-29 (0.13 U ml\(^{-1}\)) and CEA (0.05 ng ml\(^{-1}\)) | Li et al. (2015)                     |
| CA15-3         | Breast                   | Luminescent        | 39.2 and 89 μμ/ml\(^{-1}\) for CA15-3 and CA72-4, respectively | Ashbaghian-Namin et al. (2021)       |
| Ferritin       | Liver                    | SERS               | 0.41 pg/ml                           | Ma et al. (2020)                     |
| HE4            | Ovarian                  | SERS               | 10\(^{-11}\) M                      | Eom et al. (2021)                    |
| CA125          | Ovarian                  | SERS               | -                                    | TunÇ and Susatpo, (2019)             |
| Apolipoprotein A1 | Ovarian               | Luminescent        | -                                    | Garcia et al. (2021)                 |
| BRAF V600E     | Colon                    | SERS               | 1–5,000 fmol                         | Yu et al. (2020)                     |
sensitivity by signal amplification of refractive index changes/EW absorption phenomenon changes, rapid detection time, high resolution, and real-time label-free sensing. Although a greater theoretical understanding of the plasmonic shaping in AuNPs, innovative gold nanostructures and nanohybrid structures, dielectric media RI and nanostructured material production are needed for future ultrasensitive plasmonic nano-sensors for point-of-care (POC) applications (Li et al., 2014).

SERS enhancement on the high curvature tips and edges of anisotropic Au NPs, such as NSTs, has recently been employed to increase detection sensitivity. SERS Au NSTs (malachite green isothiocyanate as the Raman reporter) and an Au triangular nanoarray were utilized to develop a novel test with great sensitivity. By trapping sandwich nanoparticles over the gold triangular nanoarray and increasing the electromagnetic field intensity and 3D space, protein biomarkers produce a limited hot spots in the SERS immunosensor, which dramatically amplifies the Raman signal. The linear range of this SERS immunosensor for human immunoglobulin G protein in the buffer solution is 0.1 pg/ml to 10 ng/ml, and the detection limit is low (7 fg/ml) (Li et al., 2013). Table 3 lists some of the AuNPs-based optical biosensors that have been developed as cancer protein biomarkers.

8 CONCLUSION AND PERSPECTIVES

The discovery of peripheral biomarkers that are linked to cancer treatment grows as the disease progresses. Tumor cells, vesicles, nucleic acids, and proteins are all examples of this. The detection and prognosis of cancer patients can be improved by using biomarkers that circulate in the bloodstream. As a result, better detection methods are critical. Flow cytometry, ELISA, and DNA and protein arrays, among other standard analytical methods, have played a critical role in this field’s advancement. Because of a lack of sensitivity, they are ineffective for cancer screening and diagnosis. Biomarker classification has been made easier thanks to the wide variety of nanotechnology-based approaches that have been developed. It has been possible to develop several other tests using AuNPs, including those that use LSPR and colorimetry in addition to SERS and fluorescence. There are numerous uses for each of them, depending on the goal and the technique of reading the signal. AuNP-based optical sensing systems can be used in mobile, wearable, and even implantable devices. For long-term sustainability, AuNPs must be established on a broad scale and in a variety of environments. Reduced analysis time and prevention of non-specific adsorption of biomolecules onto AuNPs are two further ways to improve the analytical performance of biosensors. To better understand the biodistribution and clearance of AuNPs used in biomedical imaging, more research is needed. Additionally, new targeting agents and targeting strategies are needed to improve molecular imaging’s specificity. Investigating the creation of AuNP composites or hybrids with other nanoparticles is vital to discovering the potential for new research and application prospects. Multifunctional AuNPs and nanohybrids based on AuNPs are likely to be increasingly important in the near future in relation to multi-antalyte imaging.

AUTHOR CONTRIBUTIONS

JT and SD compiled the data and designed the manuscript. LR further improved the manuscript, edited and submitted it to the journal. All authors reviewed and approved the final version.

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