Impact of Pore−Walls Ligand Assembly on the Biodegradation of Mesoporous Organosilica Nanoparticles for Controlled Drug Delivery

Haneen Omar, † Basem Moosa, † Kholod Alamoudi, † Dalaver H. Anjum, ‡ Abdul-Hamid Emwas, ‡ Omar El Tall, § Binh Vu, § Fuyu Tamanoi, § Abdulaziz AlMalik, *∥ and Niveen M. Khashab *†, †

† Smart Hybrid Materials Laboratory, Advanced Membranes, and Porous Materials Center, King Abdullah University of Science and Technology, Thuwal 23955-6900, Saudi Arabia
‡ King Abdullah University of Science and Technology (KAUST), Core Labs, Thuwal 23955-6900, Saudi Arabia
§ Department of Microbiology, Immunology and Molecular Genetics, Jonsson Comprehensive Cancer Center, Molecular Biology Institute, University of California, Los Angeles, California 90095-1489, United States
∥ Life Sciences and Environment Research Institute, Center of Excellence in Nanomedicine (CENM), King Abdulaziz City for Science and Technology (KACST), Riyadh 11461, Saudi Arabia

Supporting Information

ABSTRACT: Porous materials with molecular-scale ordering have attracted major attention mainly because of the possibility to engineer their pores for selective applications. Periodic mesoporous organosilica is a class of hybrid materials where self-assembly of the organic linkers provides a crystal-like pore wall. However, unlike metal coordination, specific geometries cannot be predicted because of the competitive and dynamic nature of noncovalent interactions. Herein, we study the influence of competing noncovalent interactions in the pore walls on the biodegradation of organosilica frameworks for drug delivery application. These results support the importance of studying self-assembly patterns in hybrid frameworks to better engineer the next generation of dynamic or “soft” porous materials.

1. INTRODUCTION

Controlling periodicity in hybrid porous structures has bestowed infinite practical utilities, especially in the fields of separation, encapsulation, and catalysis.1−3 The crystalline features of molecularly ordered hybrid structures, such as metal−organic frameworks (MOFs), made these materials quite superior to their amorphous counterparts.4 Periodic mesoporous organosilica (PMOs) are a class of inorganic−organic hybrid porous materials that have crystal-like pore walls with structural periodicity. It is synthesized by direct condensation of the bridged organosilane precursor (R′O)3Si−R−Si(OR′)3, where R is the organic bridging group.5−8 Inagaki et al. reported the first periodic organosilica with lamellar ordered pore walls employing a benzene organic bridge.9 Supramolecular structures formed by self-directed assembly in trans or cis isomers of azobenzene has also been reported.10−13 More recently, hydrogen bonding in cyclo-hexane triamide caused a new type of molecular-scale ordering within the pore wall, which improved the guest loading efficiency in these hybrid structures.14 Engineering ordered porous structures employing noncovalent interactions rather than metal coordination is quite intriguing, as it can produce a new generation of hierarchical and dynamic porous structures especially for biomedical applications.14

Many degradable PMOs have been designed that can be triggered by light,14 enzyme (GTH, trypsin),15,16 pH,17 and electrostatic interaction18 to controllably release the therapeutic cargo. Moreover, loading guest organic molecules in the pores does not need a capping agent because of the hydrophobic interaction between the guest and organic pore wall.19 Enzymatic triggers are highly thought after because of their selectivity and site specificity.20,21 The azo-bond is an interesting moiety to employ in a biodegradable drug delivery system, as it reductively cleaves in the presence of azoreductase.22−25 Moreover, this bond could be effectively cleaved by one-electron reduction which is applicable only
under hypoxia conditions. In addition, azoreductase was used as a trigger to visualize specifically lysosomes in hypoxic cancer cells. Many drug delivery systems were reported using this building block as a trigger such as MOFs, polymeric vesicles, and hydrogels.

In this work, we study the influence of ligands self-assembly on the biodegradation of mesoporous organosilica nanoparticles (NPs) for on-demand drug delivery. Azobenzene linkers (AZO) were condensed with aromatic benzene (B) or aliphatic ethane (E), bridging groups to prepare the hybrid frameworks AZO-B and AZO-E, respectively (Figure 1).

Investigating the ligand packing on both frameworks showed that AZO-B afforded a framework with a compact pore wall compared with AZO-E. Interestingly, AZO-B showed a faster biodegradation than AZO-E in vitro and in vivo. We expect that other hybrid structures can be produced in a fashion similar to tailor pore wall chemistry and enable the preparation of soft hybrid frameworks with site-specific conjugation and degradation.

2. RESULTS AND DISCUSSION

Polycondensation of diazobenzene-triethoxysilyl amide (165 µL, 0.20 mmol) under basic conditions with benzene (400 µL, 1.0 mmol) or ethane-modified silanes (250 µL, 1.0 mmol) followed by extraction with an alcoholic solution of ammonium nitrate (6 g L⁻¹) and drying overnight afforded NPs AZO-B and AZO-E, respectively. Azobenzene may form multiple noncovalent interactions depending on the neighboring molecules, and the dynamic nature of the azo bond makes it more susceptible to degradation. Increasing the percentage of azobenzene beyond 15% afforded bulk samples at the microscale with a more complex pore wall packing. The AZO linker 1 was prepared following Scheme S1 and fully characterized using ¹H and ¹³C NMR (Figure S1). The TEM images of AZO-B and AZO-E reveal well-ordered arrangements of mesoscopically ordered pores with a hexagonal symmetry (Figures S2a,b and S3a,b, respectively). The chemical composition of AZO-B and AZO-E NPs was confirmed by scanning TEM (STEM) combined with electron energy loss spectroscopy (EELS) and energy dispersive X-ray spectroscopy (EDX) (Figures S2h,i and S3h,i, respectively). The STEM–EELS validated the homogeneous distribution of the azo precursor within AZO-B and AZO-E frameworks by the elemental mappings of silicon, oxygen, nitrogen, and carbon (Figures S2c–g and S3c–g, respectively). EDX spectroscopy also confirmed the presence of silicon, oxygen, carbon, and nitrogen elements (Figures S2i and S3i). Fourier transform infrared spectroscopy (FT-IR) verified the successful incorporation of AZO in the framework of AZO-B where the characteristic peaks of silica [νSi–O (1090–1125 cm⁻¹)] and the νC–H and νSi–C stretching vibration modes of the benzene group at 3070 and 1162 cm⁻¹ were observed (Figure S4). The vibrational spectra of azobenzene were detected in the 1650–900 cm⁻¹ region, and the out-of-plane aromatic δCsp²–H bending was detected at 334 cm⁻¹ (Figure S4). Similarly, FT-IR of AZO-E showed the ethane modes νSi–C and aliphatic νC–H at 1162 and 2908 cm⁻¹ and the δCsp²–H at 918 cm⁻¹ along with the stretching mode of νSi–O from 1090 to 1125 cm⁻¹ (Figure S4). Solid-state ¹³C and ²⁹Si magic angle spinning (MAS) NMR measurements of AZO-B showed a successful incorporation of organic moieties into the mesostructured NPs with a degree of condensation of ca. 70% (Figure 2a).

The NMR spectrum of AZO-B shows the peaks at −59, −68, and −77 ppm, corresponding to T¹(CSi(OSi)(OH)₂), T²(CSi–(OSi)₂(OH)), and T⁴(CSi(OSi)₃), respectively, in addition to a small peak at −108 ppm attributable to Q⁴(Si(OSi)₃), suggesting that the condensation has proceeded. The ¹³C NMR spectrum was dominated by a peak at 135 ppm, which corresponds to the superposition of unresolved signals from o- and m-carbons in the phenylene ring (Figure 2b). There were two additional peaks at 30 and 53 ppm, which were assigned to aliphatic groups (Si–O–CH₂CH₃). The ²⁹Si MAS NMR...
spectra of AZO-E exhibited two resonances with a degree of condensation of ca. 84% (Figure 2a). The first resonance (−71.6 ppm) was attributed to T2(CSi(OSi)2(OH)), a partially condensed silica species with one hydroxyl group and the other (−80.7 ppm) was assigned to T3(CSi(OSi)3), a fully condensed silicon with three siloxane bonds.39 Virtually, no peak was detected for SiO4 species (Si sites attached to four oxygen atoms Qn, n = 1−4) between −98 and −111 ppm, indicating essentially no evidence for Si−C bond cleavage during the sol−gel processing and synthesis.40 The 13C MAS NMR spectrum showed the presence of a signal at 5 ppm (Figure 2b). This is due to the −CH2−CH2− groups covalently linked to two Si atoms.41,42

XRD analysis was performed to study the structure arrangement and phase purity of the AZO NPs. The low-angle XRD patterns for AZO-B and AZO-E show dominant diffraction peaks (100) at 2θ = 2.2 with a spacing of d = 4.02 nm and 2θ = 1.74 with a spacing of d = 5.08 nm, indicating a two-dimensional hexagonal symmetry (p6m) of the materials (Figure 3).43 The corresponding lattice constants of the (100) reflection were found to be 4.65 nm for AZO-B and 5.87 nm for AZO-E, which support the mesoscale-periodicity of the NPs.9,43 AZO-B low-angle XRD spectrum shows two additional diffraction peaks, which can be indexed as (110) and (200) reflections as shown in Figure 3a. The high-angle XRD patterns of AZO-B displayed additional three diffraction peaks at 2θ = 11.6°, 23.4°, and 35.4° which equates to d = 0.76, 0.38, and 0.25 nm, respectively (Figure 3b).

Nitrogen adsorption−desorption of AZO-B and AZO-E showed type IV isotherm, which is characteristic of a mesoporous material (Figure S5).44 The structural information on both systems is listed in Table S1. The AZO-B-specific surface area, pore volume, and pore size were 1211 m²/g, 0.84 cm³/g, and 1.6 nm, respectively. The AZO-E shows an increase in the pore size to 2.7 nm, but the specific surface area and pore volume are comparable to AZO-B (1190 m²/g and 0.85 cm³/g, respectively). These results suggest that the AZO linker plays a significant role in controlling the pore size of the NPs. The pore size distribution of the materials was obtained by the Barrett−Joyner−Halenda method.45 Both samples have uniform pore size distributions with a dominant peak center at 1.6 nm for AZO-B and 2.7 nm for AZO-E, which is in agreement with the pore dimensions estimated from the high-resolution TEM images. The measured pore width by TEM was about 2−3 nm, which is in good agreement with the nitrogen isotherm results.

Biodegradation of NPs has recently become a hot research topic because of the impact of these lingering nanoplatforms on the environment and general health. Hundreds of nano-formulations exist in the market predominantly in the personal care and cosmetics industry. Crystallinity and order in these systems have proved crucial for their toxicity and consequently intended use.46 Targeted drug delivery is also an important application of enzymatically degradable NPs.47 We thus tested

Figure 3. (a) Low- and (b) high-angle XRD patterns of AZO-B and AZO-E samples.

Figure 4. TEM images of (a) AZO-B and (b) AZO-E before and after degradation in azoreductase enzyme in the presence of NADPH for 3 and 24 h.
the biodegradation of AZO-B and AZO-E to verify the effect on decomposition. Mimicking a reducing tumor microenvironment, a biological media containing the azoreductase enzyme in the presence of coenzyme NADPH was used in this study. Azoreductase can reductively cleave the azo-bond and has been used enormously in colon-specific drug delivery systems such as a prodrug sulfasalazine.\textsuperscript{48–55} The biodegradation of AZO-B and AZO-E in the azoreductase enzyme was monitored by TEM over a period of 24 h (Figure 4). Interestingly, AZO-B degraded faster than AZO-E, which may be attributed to the relatively smaller pores. Although such assemblies are considered more stable, the close proximity of bonds interacting with the active site of the azoreductase enzyme might be enhancing the rate of biodegradation.

We then tested biocompatibility and the utility of such system in targeted drug delivery. Colon cancer cells, HCT-116 cells, were used for all in vitro testings. Both AZO-B and AZO-E exhibit no significant cytotoxicity against HCT-116 cells at a high concentration of 100 μg/mL (Figure 5). However, AZO-E showed a safer profile where 95% of the cells were viable at a NP concentration of 100 μg/mL compared with 60% when AZO-B was used.

![Figure 5. Cell viability in colon cancer (HCT-116) cells of AZO-B and AZO-E.](image)

Both systems were then loaded with the anticancer drug doxorubicin (DOX) and tested in physiological media before in vitro incubation with HCT-116 cells. The release experiments were carried out in the presence and absence of the azoreductase enzyme and NADPH coenzyme. Figure 6a shows that DOX release was initiated by the presence of the azoreductase enzyme. A negligible amount of DOX was released in the absence of the enzyme, and the system was not leaking as can be concluded from the release profile (Figure 6a). DOX was efficiently loaded in AZO-NPs, and incubation of AZO-B and AZO-E with HCT-116 cells showed efficient uptake and delivery of DOX into cancer cells under hypoxic conditions (Figure 6b). Confocal laser scanning microscopy (CLSM) images showed an increase in red fluorescence of DOX molecules when AZO-NPs were used, which is in agreement with the drug release profile that showed a higher drug release profile for AZO-B compared with AZO-E. Furthermore, 3D intracellular fluorescence reconstruction of the uptake and delivery is presented in Figure S6. As a control, AZO-B and AZO-E were incubated with HCT-116 cells in the absence nonhypoxic conditions and showed no drug release because of negligible amounts of NP degradation.

![Figure 6. (a) DOX release profiles of AZO-B and AZO-E in the absence and presence of the azoreductase enzyme. (b) CLSM images of HCT-116 cells incubated with DOX loaded AZO-B and AZO-E under hypoxia for 1 h. Nuclei are stained in blue with Hoechst 33342 dye, NPs appear with the green fluorescence (fluorescein isothiocyanate) and DOX fluorescence in cells (red).](image)

Chicken embryos were transplanted with OVCAR-8 ovarian cancer cells, expressing green fluorescent protein. Loaded NPs with DOX were injected into the blood vessels followed by daily monitoring of tumor sizes relative to controls. Figure 7 shows that the injection of drug-loaded NPs has potent antitumor activity without any other toxic effects on organs. Administration of NPs loaded with DOX results in a dramatic tumor shrinkage relative to control over time. AZO-B showed a drastic decrease in the tumor size just after two days of injection compared with AZO-E, while safely retaining the function of all other organs.

![Figure 7. (a) Actual and (b) visible light fluorescence images of chicken egg tumor transplanted with OVCAR-8 cells before and after injection with DOX-loaded AZO-B and AZO-E.](image)

### 3. CONCLUSION

Studying pore wall packing will lead to interesting hybrid platforms that can be smart in nature. This molecular scale ordering will drastically influence the properties of these frameworks. Engineering materials to have a different pore size is well established. However, we need to investigate the overall
properties of these materials, especially when it comes to stability and responsiveness. In this work, we showed that closer pore packing in AZO-B enhanced the enzymatic biodegradation of these hybrid frameworks compared with AZO-E. Understanding pore wall packing and assembly of linkers within the space will lead to superior porous materials that can make it closer to scale-up and eventual market use.

4. EXPERIMENTAL SECTION

4.1. Materials and Methods. Cetyltrimethylammonium bromide (CTAB), 1,4-bis(triethoxysilyl)benzene, 1,2-bis-(trimethoxysilyl)ethane, 4-nitrobenzoic acid, glucose, thionyl chloride, tetrahydrofuran (THF; anhydrous, ≥99.9% (dry THF)), trimethylamine, and 3-aminopropyltriethoxysilane were purchased from Sigma-Aldrich. Sodium hydroxide (NaOH) and phosphate buffered saline [(10x), pH 7.4] were purchased from Fisher. Milli-Q water was used in all synthetic experiments. All chemicals were used without further purification.

4.2. Instrumentation. Powder XRD measurements were performed using a PANalytical X’Pert Pro X-ray powder diffractometer using the Cu Ka radiation (40 V, 40 mA, λ = 1.54056 Å) in a θ-2θ mode from 20° to 90° (2θ). TEM images, EELS, and EDX were recorded using a Tecnai 12 T (FEI Co.) microscope operated at 120 kV. The GIF was used in the EELS mode in conjunction with high angle annular dark field—STEM. Nitrogen adsorption—desorption isotherms were acquired using a Micromeritics ASAP 2420 instrument. 1H NMR and 13C NMR spectra were performed at 500 MHz with CDCl3 solutions with an AVANCE III Bruker Corporation instrument. For solid NMR spectra were carried out by using a Bruker 400 MHz AVANCE III NMR spectrometer (resonating at 100.64 MHz for 13C and 79.514 MHz for 29Si) equipped with double resonance 4 mm Bruker MAS probe (Bruker BioSpin, Rheinstetten, Germany). To be able to spin the samples were finely ground then packed evenly into 4 mm zirconia rotor and sealed at the open end with a Vespel cap. The 29Si spectra were recorded with 14 kHz spinning rate using one pulse program from Bruker standard pulse library with 30° flipping angle with recycle delay time of 30 s. The 13C spectra were recorded using cross polarization CP MAS experiments using the CP pulse program. Each 13C NMR spectrum was recorded by collecting 12k scans while the 29Si NMR spectrum was recorded with 4k scans at room temperature. Bruker Topspin 3.2 software (Bruker BioSpin, Rheinstetten, Germany) was used for data collection and analysis. FT-IR spectra were recorded using a Thermo Scientific spectrometer ( Nicolet iS10). Absorption spectra were recorded using a Varian Cary 5000 spectrophotometer, and fluorescence data were collected using a Varian Cary Eclipse fluorimeter.

4.3. Synthesis of AZO-B and AZO-E NPs. A mixture of CTAB (250 mg, 0.68 mmol), distilled water (120 mL), and NaOH (875 μL, 2 M) was stirred at 85 °C for 30 min in a 250 mL round-bottom flask. The azo precursor (165 μL, 0.20 mmol) was added to the solution, followed by 1,4-bis-(triethoxysilyl)benzene (400 μL, 1.0 mmol), and the condensation process was conducted for 2 h at 85 °C. After that, the solution was cooled to room temperature under stirring. The sample was then extracted by using ultrasonic bath with an alcoholic solution of ammonium nitrate (6 g L−1) at 45 °C for 30 min and washed three times with ethanol, water, and ethanol. The as-prepared material was dried under vacuum. The synthesis of AZO-E NPs was synthesized as described for the AZO-B NPs above with an 1,2-bis-(trimethoxysilyl)ethane precursor (250 μL, 1.0 mmol) instead of the 1,4-bis(triethoxysilyl)benzene precursor.

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsomega.8b00418.

Detailed procedures for the preparation of AZO precursor, loading, release profile, in vitro and in vivo studies, and all characterization techniques (PDF)

AUTHOR INFORMATION

Corresponding Authors
*E-mail: aalmalik@kacst.edu.sa (A.A.).
*E-mail: niveen.khashab@kaust.edu.sa (N.M.K.).

ORCID
Basem Moosa: 0000-0002-2350-4100
Niveen M. Khashab: 0000-0003-2728-0666

Notes
The authors declare no competing financial interest.

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