Retinal Thickness Normative Data in Wild-Type Mice Using Customized Miniature SD-OCT

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Abstract

Objective: To report normative data for retinal thickness in wild-type C57BL/6 mouse utilizing a miniature SD-OCT system.

Methods: Thirty adult mice (range: 3–5 months) were anesthetized and secured into the Bioptigen Spectral Domain Ophthalmic Imaging System. Right eye SD-OCT images were standardized by centralizing the optic nerve head (ONH) prior to image acquisition. Global and quadrant total retinal thickness (TRT) values were measured from retinal nerve fiber layer to retinal pigment epithelial layer. Posterior segment analyses also included the outer retinal layer (ORL) and inner retinal layer (IRL). Further sublayer analyses of four layers from the ORL and three layers comprising the IRL were also performed.

Results: The overall mean±SD global TRT in a C57BL/6 mouse model was 204.41±5.19 µm. Quadrant mean TRT values were 204.85±5.81 µm inferiorly, 204.97±6.71 µm nasally, 205.08±5.44 µm temporally, and 202.74±4.85 µm superiority. Mean±SD thickness for ORL and IRL were 126.37±10.01 µm, and 107.03±10.98 µm respectively. The mean±SD estimates for the four layers of the ORL were 18.23±2.73 µm, 26.04±4.21 µm, 63.8±6.23 µm, and 19.22±4.34 µm. Mean±SD values for the three IRL sublayers were 27.82±4.04 µm, 59.62±6.66 µm and 19.12±3.71 µm.

Conclusion: This study established normative values for the total retinal thickness and sublayer thickness for the wild-type C57BL/6 mice. Moreover, it provides a standard of retinal morphology, in a commonly used animal model, for evaluating therapeutic interventions and retinal disease pathophysiology.

Introduction

Spectral domain optical coherence tomography (SD-OCT) is an important imaging modality in clinical ophthalmology and vision science for characterizing morphology and understanding pathophysiological changes within the retina. The rapid, high resolution, non-invasive cross-sectional images produced by SD-OCT is an important tool for diagnosing and monitoring posterior segment pathology longitudinally [1,2].

Mouse models have been instrumental for understanding pathophysiology in a variety of retinal diseases [3–21]. Historically, ex vivo histological sectioning is used to study retinal disease in mouse models. Inherent methodological limitations confound tissue integrity and curtail longitudinal evaluations within a single subject. With the advent of in vivo applications such as fundoscopy, confocal scanning laser ophthalmoscopy (cSLO), angiography, electroretinography (ERG), and optical coherence tomography (OCT), limitations associated with ex vivo histological preparations can now be circumvented. Although SD-OCT provides non-invasive histological – grade sections of the rodent posterior segment, image acquisition is technologically cumbersome as human devices are retrofitted for animal use.

Hand-held spectral domain ophthalmic imaging system (SDOIS) (Bioptigen, Inc., Durham, NC) represents an alternative non-invasive in vivo imaging device. It contains the animal imaging mount with rodent alignment stage (a unique platform with adjusting that stereotactically secures mice within a cassette while mounted to a rotational stage) and a hand-held 840 nm SD-OCT probe (HHP) capable of axial resolutions of 5 micrometers (µm) [22–25]. Bioptigen SD-OCT technology is increasingly implemented in rodents [26] for biometrical analysis as well as evaluation and management of retinal disorders. However, data on normative values of the retina for wild-type C57BL/6—a common mouse model for the study of retinal diseases – is not available. The overall goal of this study is to report normative SD-OCT data of the mouse retina with the Bioptigen SDOIS.

Methods

Ethics Statement

All experiments were performed in compliance with the University of Florida institutional animal care and use committee (IACUC) guidelines and/or adhered to the Association for Research in Vision and Ophthalmology Statement for the Use of Animals in Ophthalmic and Vision Research. This study was reviewed and approved by the University of Florida IACUC. All animals were managed in accordance with the University of
Florida animal care services (ACS) rodent handling procedures. Animal wellbeing and welfare were monitored daily by the ACS staff and the study investigators. Ketamine/Xylazine anesthetic mixture was used to sedate animals during scanning in order to minimize distress. During the course of this study, no animal was sacrificed or showed signs of suffering.

**Animals**

Thirty adult C57BL/6 mice (Jackson Laboratory, Bar Harbor, ME) between the ages of three to five months were utilized for this study. All mice were housed and maintained in the University of Florida ACS facility. The mice were adherent to a 12-hour light/dark cycle with open access to feed and water. Animal preparation
and SD-OCT scanning were performed in an ACS-designated and approved procedural location.

SD-OCT Imaging

Mice were anesthetized with a mixture of Ketamine (Ketaject; 80 mg/kg; Webster Veterinary, Devens, MA) and Xylazine (Ana Sed; 10 mg/kg; Webster Veterinary; Devens, MA) delivered via intraperitoneal injection to ensure restriction of movement during optical scanning. Both pupils were dilated with topical Tropicamide (1%; Akorn Inc.; Lake Forest, IL). To prevent corneal desiccation during procedure, topical Systane Ultra® lubricant eye drop (Alcon, Fort Worth, TX) was applied bilaterally every minute. Following dilation and lubrication, the mice were positioned into the AIM-RAS setup (Figures 1a &1b), which permitted X, Y, and Z axis manipulation for proper alignment of mouse eye with HHP bore in order to properly center and visualize the ONH within the viewing panes for B-scan and en-face images.

In order to achieve ONH centering during imaging, the geometrical working distance between the subject eye and the HHP bore was acquired by an aiming tip and aiming target calibration method prior to mouse insertion into AIM-RAS apparatus. The working distance between the SD-OCT lens and the mouse eye was approximately 5 mm. In order to maintain central arrangement prior to SD-OCT image capture, the ONH was repositioned vertically by clockwise and counter clockwise movement.

Figure 2. (a) C57BL/6 mouse en-face scan showing the central optic nerve head; (b) showing the 1 mm diameter (arrows) within and around central retinal subfield (CSF); (c) the retinal quadrants surrounding CSF with overall mean (±SD) total retinal thickness; (d) a B-scan image from equatorial slice of en-face scan showing the different sublayers that were measured using the manual calipers. [ORL, outer retinal layer; IRL, inner retinal layer; RPE, retinal pigment epithelium; ELM/IS/OS, external limiting membrane/inner segment of photoreceptors/outer segment of photoreceptors; ONL, outer nuclear layer; OPL, outer plexiform layer; INL, inner nuclear layer; IPL/GC, inner plexiform layer/ganglion cell; RNFL, retinal nerve fiber layer].

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animal cassette rotation and horizontally by swiveling the mouse cassette towards the nasal or temporal locations. Careful attention was paid to accurate focusing of the image at the time of manual calibrations to the RAS and mouse cassette. Once image acquisition commenced, the scans were performed in rapid succession without need for further manipulation of the mice. The imaging protocol entailed a 3 mm perimeter square scan sequence producing a single en-face image of the retina through a 50-degree field of view from the mouse lens, following mydriasis. The en-face image comprised of 100 B-scan tomograms with each B-scan consisting of 1000 A-scans.

All scans were performed by one of two operators (LRF or JMD). B-scan slices were recorded only if posterior segment layers could clearly be set with standard image display options for both image brightness and contrast. SD-OCT scans were not recorded if retinal vasculature cross-sections were visualized within any of the measured segment layers. The en-face image was transected centrally along the ONH in order to provide a B-scan image of the retina layers at this location (Figure 2a). The ONH was used as the landmark with central subfield (CSF) scan diameter of approximately 1 mm (Figure 2b).

### Analysis of SD-OCT Imaging

The SD-OCT B-scan cross-sectional images were analyzed with the InVivoVue Clinic software incorporated with the SDOIS. The software included ‘manual calipers’ that could be used for measurements in microns (μm) of the various posterior segment sublayers. Retinal en-face scans were divided into inferior, nasal, temporal, and superior quadrants surrounding the retinal CSF containing the ONH (Figure 2c). The total retinal thickness (TRT) was defined as the width from the RNFL to the RPE layer, including both layers. Four measurements were made on the same scan and averaged. Within the center of each quadrant, three B-scans separated by approximately 150 μm were used for measurements. Hence, 12 points were used for each quadrant to average the retinal thickness measurements.

### Table 1. Mean Total Retinal Thickness and Sublayer Thickness ± Standard Deviation (μm).

| Animal | TRT-I | TRT-N | TRT-T | TRT-S | TRT-Global |
|--------|-------|-------|-------|-------|------------|
| 1      | 204.17| 203.67| 204.00| 198.83| 202.92     |
| 2      | 204.33| 204.67| 206.67| 200.00| 203.42     |
| 3      | 203.33| 203.67| 203.00| 202.17| 203.04     |
| 4      | 202.67| 203.33| 201.00| 199.83| 202.96     |
| 5      | 203.17| 201.00| 206.67| 202.33| 203.54     |
| 6      | 205.00| 205.67| 204.33| 200.83| 203.96     |
| 7      | 199.00| 197.33| 197.00| 195.50| 197.96     |
| 8      | 197.67| 194.33| 194.00| 192.33| 193.54     |
| 9      | 198.33| 196.00| 202.00| 194.50| 196.54     |
| 10     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 11     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 12     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 13     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 14     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 15     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 16     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 17     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 18     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 19     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 20     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 21     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 22     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 23     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 24     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 25     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 26     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 27     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 28     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 29     | 191.00| 190.00| 190.00| 185.00| 189.54     |
| 30     | 191.00| 190.00| 190.00| 185.00| 189.54     |

After determining the total retinal thickness in the retinal quadrants, measurements were made for the outer retinal layer and inner retinal layer. Further, retinal thickness sub-analyses were done to measure each individual layer of the outer and inner retina (Figure 2d) with manual calipers in the following order: outer retina – retinal pigment epithelium (RPE), external limiting membrane/inner segment of photoreceptors/outer segment of photoreceptors (ELM/IS/OS), outer nuclear layer (ONL), outer plexiform layer (OPL); inner retina – inner nuclear layer (INL), inner plexiform layer/ganglion cell (IPL/GC), and the retinal nerve fiber layer (RNFL). Although the recording of the scans were done on a single day for each mouse, the measurement of the TRT and the retinal thickness sub-layers were done at different times.
Statistical Analysis
Mean and standard deviation (± SD) were calculated for the within-subject triplicate measurements from each layer of the posterior segment. The mean (± SD) between subject values for the posterior segment layers were then computed. Students’ T-test was used to calculate statistical significance and a p-value less than 0.05 was considered significant. We looked at the interobserver variability between two independent observers (LRF and WL) using two methods: first, by measuring TRT for all animals, and then the sublayer thickness values from ten randomly selected animals. The mean difference and 95% confidence interval (CI) for interobserver measurements were estimated. A two-way mixed effect intraclass correlation (ICC) assessment (SPSS.21) was used to measure interobserver agreement. Bland-Altman plots were constructed to assess the degree of interobserver agreement for TRT and sublayer measurements.

Results
Retinal thickness measurements from a total of thirty adult mice eyes were analyzed. Globally, the mean±SD TRT value for all study mice was 204.41±5.19 μm (Table 1). The four outer quadrant retinal areas surrounding the CSF region had mean retinal thickness values of 204.85±5.81 μm inferiorly, 204.97±6.71 μm nasally, 205.08±6.71 μm temporally, and 202.74±4.85 superiorly. The overall mean thickness for the outer retina and inner retina were 126.37±10.01 μm, and 107.03±10.98 μm respectively. Thickness values for the retinal sublayers were: RPE = 18.23±2.73 μm; ELM/IS/OS = 26.04±4.21 μm; ONL = 62.8±6.23 μm; OPL = 19.22±4.34 μm; INL = 27.82±4.04 μm; IPL/GC = 59.62±6.66 μm; RNFL = 19.12±3.71 μm (Table 1).

Table 2 shows the mean global TRT and the retinal thickness in the four quadrants in each animal. Similarly, Table 3 depicts the mean retinal thickness of different sublayers in each animal.
remarkable consistency with layer measurements (Figure 4). excellent interobserver agreement with an ICC value of 0.99 sublayer retinal thicknesses, as shown in Table 4. Again, there was observer difference for total retinal thickness (TRT) measure-
ments in the nasal quadrant of all animals (n = 30).

Discussion

SD-OCT technology has expanded the boundaries of vision science as it relates to non-invasive imaging of human retina. In human studies, SD-OCT normative values have been established for macular thickness [27,28] and its sublayers [29]. This has served to further enhance the understanding of retinal architecture and structural deficits. With the use of SD-OCT, multiple, reproducible, high-resolution scans, accuracy in identifying defects at the micron level has improved. Moreover, serial imaging over time has also helped in studying the course of diseases and their prognoses.

Similarly, although the advent of this technology has heralded a revolution for animal study in vision science, normative database from a ubiquitous small animal species used to model the human eye has not been established. Various groups have assessed mouse TRT and retinal sublayers by utilizing different imaging setups. Some have measured these layers with retrofitted human SD-OCT devices coupled with an external lens to neutralize mouse corneal optical power [22,23]. Other groups have incorporated custom-designed SD-OCT instruments that maintain resolution capabilities, while eliminating the need for external lens, when imaging rodent retinas [23,25,26].

In this present study, we determined the mean TRT measurement for the four retinal quadrants surrounding the ONH. Additionally, our findings included the mean thickness values for the individual layers that comprise the posterior segment in the C57BL/6 mouse strain, while utilizing a miniaturized SD-OCT with stereotactic multi-axis rotational rodent containment device (i.e., Biopigen SDOIS).

In terms of TRT for the four retinal quadrants surrounding the ONH, our data suggest that there is uniformity in measurement value. Despite not reaching a significant difference, the superior retina region (202.74 ± 4.85 μm) showed a trend of being the thinnest region as compared to inferior (204.85 ± 5.81 μm), nasal (204.97 ± 6.71 μm), and temporal (205.08 ± 5.44 μm) areas. We estimated that the TRT for the C57BL/6 mouse – as extrapolated from averages of quadrant measurements – to be 204.41 ± 5.19 μm. The results from our study are consistent with those obtained by previous groups [25,30]. There have been other investigators who have shown mean TRT values ranging from 200–250 μm [22,30,31]. However, the measurement values obtained by Gabriele et al. (2010) [26] overestimates all prior mentioned reports. In addition to assessing global TRT, their report was the first to examine quadrant TRT in the C57BL/6 mouse. They employed a similar SD-OCT device, as in our study (Biopigen Inc., Durham, NC), to generate en-face volumetric images, centered at the ONH. In the Gabriele et al. study, automated segmentation software was used to measure B-scan TRT spanning from the inner limiting membrane (ILM) to the RPE. Global and quadrant TRT outcome measurements were estimated by applying a linear mixed-effects statistical model. From their analyses, the authors reported that the mean global TRT was 298.21 μm [26]. Moreover, they showed the superior retina (310.38 μm) as being the thickest quadrant in comparison to the inferior (291.55 μm), nasal (296.52 μm) and the temporal (294.37 μm) areas. Higher TRT values obtained in that study could potentially be attributed to the region of selection indicated by automated segmentation. Although Gabriele et al. selected boundary points that supposedly corresponded to the ILM and RPE, it is possible that the choroid was factored in when measuring the retinal distance from the ILM to the RPE (Figure 3, Gabriele et al., 2010). This inclusion could have increased the global and quadrant TRT values in their study. Another probable explanation for their overestimated TRT values could be based on
the level of resolution obtained with their B-scan images. Their scanning protocol required only 250 averaged A-scans (each an average of 4 individual A-scans) × 250 frames, whereas our scanning protocol included 1000 A-scans per B-scan with 100 accumulated B-scans with a higher resolution.

In addition to TRT measurements, we also performed sub-analyses of the thickness values for different layers of the retina. Broadly, we first analyzed the thickness of the outer retina (126.37 ± 10.41 μm) and inner retina (107.03 ± 10.98 μm). Further, we also analyzed each of the retinal layers constituting the C57BL/6 retina. Although retinal sublayer measurements were also performed in a study by Fischer et al. (2009) [23], they investigated five retinal sublayers as compared to the seven evaluated in our study. Their study showed slightly increased retinal thickness as compared to our findings. This difference could possibly be accounted for by the dissimilarity in resolution – they used a third generation, commercially available human SD-OCT apparatus versus the SDOIS Biopigen system used in our study. Another factor that could possibly account for the difference is the absence of sharp demarcation of each layer and hence, the inconsistency in defining different layer borders and their measurements. This inconsistency could be a possible explanation for the difference of about 30 μm.

In conclusion, this current study describes the normative retinal values for the C57BL/6 mouse while utilizing the Biotigen SDOIS device. It provides normative values for the total retinal thickness as well as the individual sublayers of the retina. This will serve as a standard for disease models in this mouse strain to better understand the causes of diseases, their pathophysiological mechanisms, and any treatment options that maybe available.

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Author Contributions
Conceived and designed the experiments: LRF JMD SB. Analyzed the data: LRF SG KVC. Performed the experiments: LRF JMD SB. Contributed reagents/materials/analysis tools: LRF SG KVC. Wrote the paper: LRF SG KVC.

References
1. Wojtkowski M, Srivasan V, Fujimoto JG, Ko T, Schuman JS, et al. (2005) Three-dimensional retinal imaging with high-speed ultrahigh-resolution optical coherence tomography. Ophthalmology 112: 1734–1746.
2. Alam S, Zawadzki RJ, Choi S, Gertz C, Park SS, et al. (2006) Clinical application of rapid serial fourier-domain optical coherence tomography for macular imaging. Ophthalmology 113: 1423–1431.
3. Smith LE, Wesolowski E, McLellan A, Kostyk SK, D’Amato R, et al. (1994) Oxygen-induced retinopathy in the mouse. Invest Ophthalmol Vis Sci 35: 101–111.
4. Kern TS, Engerman RL (1996) A mouse model of diabetic retinopathy. Arch Ophthalmol 114: 980–990.
5. Fett-Leichman RA, Kinosuchi R, Takeda M, Fan Z, Mohr S, et al. (2005) Vascular damage in a mouse model of diabetic retinopathy: relation to neuronal and glial changes. Invest Ophthalmol Vis Sci 46: 4281–4287.
6. Zheng L, Du Y, Miller C, Guiboutos-Khag RA, Ball S, et al. (2007) Critical role of inducible nitric oxide synthase in degeneration of retinal capillaries in mice with streptozotocin-induced diabetes. Diabetesologia 50: 1967–1969.
7. Aguilar E, Dorrell MI, Friedlander D, Jacobson RA, Johnson A, et al. (2008) Ocular models of angiogenesis. Cheresh, DA, editor, Methods in Enzymology. New York: Elsevier Inc. 44: 115–158.
8. Grant MR, May WS, Caballerio S, Brown GA, Guthrie SM, et al. (2002) Adult hematopoietic stem cells provide functional hemangioblast activity during retinal neovascularization. Nat Med 8: 607–612.
9. Pintler SJ, Baehr W (1991) Identification of a nonsense mutation in the rod photoreceptor cGMP phosphodiesterase beta-subunit gene of the rd mouse. Proc Natl Acad Sci U S A 88: 3832–3836.
10. Tan E, Wang Q, Quimbao AB, Xu X, Qaisah NM, et al. (2001) The relationship between opsin overexpression and photoreceptor degeneration. Invest Ophthalmol Vis Sci 42: 509–600.
11. Mears AJ, Kondo M, Swain PK, Takada Y, Bush RA, et al. (2001) Nrl is required for rod photoreceptor development. Nat Genet 29: 447–452.
12. Cheng H, Khanna H, Oh EC, Hicks D, Mitton KP, et al. (2004) Photoreceptor-specific nuclear receptor NR2E3 functions as a transcriptional activator in rod photoreceptors. Hum Mol Genet 13: 1563–1575.

Table 4. Interobserver Correlation In Measurement of SD-OCT Mean Retinal Thickness (μm).

| Layers | Observer 1 | Observer 2 | Mean Diff (Absolute Value) | 95% CI |
|--------|------------|------------|---------------------------|--------|
| Outer Retina Layer | 120.6 (6.25) | 111.6 (2.63) | 8.4 | 113–119 |
| Inner Retinal Layer | 96.4 (4.38) | 97.1 (5.51) | 0.7 | 95–99 |
| Retinal Pigment Epithelium | 15.3 (2.41) | 16.7 (4.03) | 1.4 | 15–17 |
| External Limiting Membrane/Inner Photoreceptor Segment/Outer Photoreceptor Segment | 39.6 (3.78) | 30.1 (6.57) | 9.5 | 32–38 |
| Outer Nuclear Layer | 54.3 (8.07) | 58.7 (6.33) | 4.4 | 53–60 |
| Outer Plexiform Layer | 13.8 (1.62) | 19.5 (3.60) | 5.7 | 15–18 |
| Inner Nuclear Layer | 27.5 (4.01) | 26.1 (3.41) | 1.4 | 25–28 |
| Inner Plexiform Layer/Ganglion Cell | 45 (6.43) | 55.7 (7.09) | 10.7 | 47–54 |
| Retinal Nerve Fiber Layer | 22.3 (8.73) | 18.4 (2.72) | 3.9 | 17–23 |

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13. Radu RA, Mata NL, Rafa A, Travis GH (2004) Light exposure stimulates formation of A2E oxiranes in a mouse model of Stargardt’s macular degeneration. Proc Natl Acad Sci U S A 101: 5928–5933.
14. Karan G, Lillo C, Yang Z, Cameron DJ, Locke KG, et al. (2005) Lipofuscin accumulation, abnormally electrophysiology, and photoreceptor degeneration in mutant ELOVL4 transgenic mice: a model for macular degeneration. Proc Natl Acad Sci U S A 102: 4164–4169.
15. Weber BH, Schrwee H, Moldlay LL, Gehrig A, White KL, et al. (2002) Inactivation of the murine X-linked juvenile retinoschisis gene, Rs1h, suggests a role of retinoschisin in retinal cell layer organization and synaptic structure. Proc Natl Acad Sci U S A 99: 6222–6227.
16. Seeliger MW, Grimm C, Strettoi E, Jaissle G, et al. (2001) New views on RPE65 deficiency: the rod system is the source of vision in a mouse model of Leber congenital amaurosis. Nat Genet 29: 70–74.
17. Pang JJ, Chang B, Hawes NL, Hurd RE, Davison MT, et al. (2005) Retinal degeneration 12 (rd12): a new, spontaneously arising mouse model for human Leber congenital amaurosis (LCA). Mol Vis 11: 152–162.
18. Ramanurthy V, Niemi GA, Reh TA, Hurley JB (2004) Leber congenital amaurosis linked to AIPL1: a mouse model reveals destabilization of cGMP phosphodiesterase. Proc Natl Acad Sci U S A 101: 13097–130982.
19. Dyer MA, Donovan SL, Zhang J, Gray J, Ortiz A, et al. (2004) Retinal degeneration in Apip1-deficient mice: a new genetic model of Leber congenital amaurosis. Brain Res Mol Brain Res 132: 208–220.
20. Pignatelli V, Cepko CL, Strettoi E. (2004) Inner retinal abnormalities in a mouse model of Leber’s congenital amaurosis. J Comp Neurol 469: 331–359.
21. Morrow EM, Furukawa T, Raviola E, Cepko CL. (2005) Synaptogenesis and outer segment formation are perturbed in the neural retina of Crx mutant mice. BMC Neurosci 6: 5.
22. Huber G, Beck SC, Grimm C, Sahaboglu-Tekgoz A, Paquet-Durand F, et al. (2009) Spectral domain optical coherence tomography in mouse models of retinal degeneration. Invest Ophthalmol Vis Sci 50: 3808–3895.
23. Fischer MD, Huber G, Beck SC, Tanimoto N, Muehlrieder R, et al. (2009) Noninvasive, in vivo assessment of mouse retinal structure using optical coherence tomography. PLoS One 4: e7507.
24. Fukushi T, Takahashi K, Shou K, Matsumura M (2001) Optical coherence tomography (OCT): findings in normal retina and laser-induced choroidal neovascularization in rats. Graefes Arch Clin Exp Ophthalmol 239: 41–46. Erratum in: Graefes Arch Clin Exp Ophthalmol 239: 307.
25. Ruggeri M, Wehbe H, Jiao S, Gregori G, Jockovich ME, et al. (2007) In vivo three-dimensional high-resolution imaging of rodent retina with spectral-domain optical coherence tomography. Invest Ophthalmol Vis Sci 48: 1800–1814.
26. Grover S, Murthy KK, Bhat VS, Chalam KV (2009) Normative data for macular thickness by high-definition spectral-domain optical coherence tomography (Spectralis). Am J Ophthalmol 148: 266–271.
27. Sabates FN, Vincent RD, Koulou P, Sabates NR, Gallimore G (2011) Normative data set identifying properties of the macula across age groups: integration of visual function and retinal structure with microperimetry and spectral-domain optical coherence tomography. Retina 31: 1294–1302.
28. Ooto S, Hangai M, Tomokoro A, Saito H, Araie M, et al. (2011) Effects of age, sex, and axial length on the three-dimensional profile of normal macular layer structures. Invest Ophthalmol Vis Sci 52: 8769–8779.
29. Cebulla CM, Ruggeri M, Murray TG, Feuer WJ, Hernandez E (2010) Spectral domain optical coherence tomography in a murine retinal detachment model. Exp Eye Res 90: 521–527.
30. Li Q, Timmens AM, Hunter K, Gonzalez-Pola G, Levin AS, et al. (2001) Noninvasive imaging by optical coherence tomography to monitor retinal degeneration in the mouse. Invest Ophthalmol Vis Sci 42: 2981–2989.