Normative Data on Spontaneous Stride Velocity, Stride Length, and Walking Activity in a Non-controlled Environment.

Margaux Poleur  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Ana Ulinici  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Aurore Daron  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Olivier Schneider  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Fabian Dal Farra  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Marie Demonceau  
CHR Citadelle: Centre Hospitalier Regional de la Citadelle

Mélanie Annoussamy  
Sysnav

David Vissière  
Sysnav

Damien Eggenspieler  
Sysnav

Laurent Servais  
University of Oxford  
laurent.servais@paediatrics.ox.ac.uk

Research

Keywords: Accelerometer, home monitoring, healthy volunteers, stride length, stride velocity

Posted Date: February 10th, 2021

DOI: https://doi.org/10.21203/rs.3.rs-178075/v1

License: This work is licensed under a Creative Commons Attribution 4.0 International License. Read Full License
Version of Record: A version of this preprint was published at Orphanet Journal of Rare Diseases on July 19th, 2021. See the published version at https://doi.org/10.1186/s13023-021-01956-5.
Abstract

BACKGROUND Normative data are necessary for validation of new outcome measures. Recently, the 95th centile of stride speed was qualified by the European Medicines Agency as a valid secondary outcome for clinical trials in subjects with Duchenne muscular dystrophy. This study aims to obtain normative data on spontaneous stride velocity and length in a non-controlled environment and their evolution over a 1-year period.

METHOD 91 Healthy volunteers (50 females, 41 males), mean age 16 years 11 months, were recruited and assessed at baseline and 12 months later. 4-stair climb, 6-minute walk test, 10-metre walk test and rise from floor were performed. Stride length, stride velocity, and the distance walked per hour were studied in daily living for one month after each evaluation.

RESULTS We observed significant positive correlations of the stride length with age and height of participants, and a significant increase of the median stride length over 1-year in children. In children, the 95th centile stride velocity was not correlated with age and was stable over a 1-year period.

CONCLUSION This study provides with data on the influence of age, height, and gender on stride velocity and length as well as the natural change over 1-year in controls.

Background

Duchenne muscular dystrophy (DMD) is a severe, rapidly progressive neuromuscular disorder characterized by muscle weakening. It has an estimated incidence of 1 in 5000 males (1). DMD is caused by out-of-frame mutations in the dystrophin gene, which leads to an absence or deficiency of the protein dystrophin and the degeneration of muscles fibres (2). The absence of dystrophin protein leads to progressive muscle necrosis, loss of independent ambulation by early adolescence, cardiomyopathy, respiratory insufficiency, and premature death in affected individuals (2). Loss of ambulation occurs generally around the age of 12. Several phase 1–3 trials have been conducted over the last 10 years in subjects with DMD (NCT01247207, NCT01540409, and NCT01826474), and four drugs have received regulatory approval: Ataluren, a small molecule that increases full-length dystrophin expression in patients harbouring a nonsense mutations (3), has been approved by the European Medicines Agency (EMA) (3). Eteplirsen, golodirsen, and casimirsen, three antisense oligonucleotides that induce skipping of exon 51, 53, and 45, respectively (4, 5), have been approved by the American Food and Drug Administration (FDA) (6, 7).

The 6-minute walk distance test (6MWT) has been used as a primary outcome in most published pivotal phase 3 trials in ambulant patients with DMD. Other outcomes used include the 4-stair climb (4SC) and functional scales such as the North Star Ambulatory Assessments (NSAA) in which participants are rated on their ability to perform standardized motor function tasks (3, 4, 8–11). In DMD, the high standardized response mean of these different outcome measures, which illustrates the power of these measures to demonstrate a change over a certain period of time, meant that pivotal trials required over 100 patients.
per group and trial durations of 18 months and 2 years (NCT02851797 and NCT02500381, respectively). To accelerate clinical development and investigate in parallel several approaches without being limited by the number of patients available, it is crucial to validate more powerful outcome measures. This is the case for DMD and for numerous other rare diseases, within or outside the neuromuscular field, such as Angelman syndrome (NCT04259281).

The last decade has seen an increase in the availability of wearable technology for continuous monitoring of health and wellbeing (12). For example, wearable devices that can be used to assess ambulation range from crude step counters to sophisticated multisensory systems (13). Unlike consumer devices, medical devices must demonstrate validated measurement accuracy, sensitivity, and specificity (14). Wearable devices have the potential to provide a complete view of a patient’s condition over a long time period by band-pass filtering day-to-day variation. Therefore, wearable devices provide a complementary approach with a major advantage over hospital-based assessments, which only provide ‘snapshots’ of a patient’s condition that can be affected by fatigue, illness, or lack of motivation.

In this context, we specifically developed a CE-marked class 1 wearable medical device that records passively, in a precise and sensitive way, upper and lower limb movements in everyday life (15, 16). From the capture of any single movement, several outcomes may be extracted. In ambulant patients, the identification and quantification of every individual stride allows for the calculation of the distribution of stride length and stride speed as well as for the analyses of different centiles such as the 95th centile stride velocity (SV95C). These variables are measured in a home-based environment over a 180-hour period and are reliable and highly sensitive to changes in ambulant patients with DMD (17).

Recently, the EMA qualified SV95C as a valid secondary endpoint in clinical trials on ambulant patients with DMD (18). Additional data are needed to qualify the measure as a primary endpoint (17). Wearable technology is or has been used in clinical trials of therapies for spinal muscular atrophy (19, 20), facioscapulohumeral muscular dystrophy (NCT02579239, NCT04004000), limb girdle muscular dystrophy type 2E (NCT02579239), centronuclear myopathy (NCT02057705), and Angelman syndrome (NCT04259281).

To properly interpret the longitudinal evolution of the SV95C over time in patient populations, it is necessary to understand the longitudinal evolution in subjects without muscle conditions within the same age range, in particular between 5 and 18 years old, which is the age range mostly targeted in clinical trials of ambulant DMD patients and during which growth or maturational factors may significantly interfere with measures (21, 22). Therefore, we conducted a longitudinal study in ambulant healthy subjects between 5 and 85 years of age to evaluate the changes in SV95C over 12 months.

**Method**

**Study design**
ActiLiège is a monocentric academic study that was conducted in the Reference Centre for Neuromuscular Disease in Liège, Belgium between July 2017 and September 2019 with grant funding from Action Duchenne. The protocol was approved by the local ethics committee in Liège (N/Ref:1646). Before inclusion, all participants or parents or legal guardians provided written informed consent for participation and publication.

Participants

The initial protocols planned to include a maximum of 130 healthy subjects to gather a distribution of about 5–10 patients per age year in children and a group of 30 adults. Given difficulties in recruiting mainly adult controls, 91 healthy subjects above the age of 5 years were finally assessed at baseline and 84 were assessed after 12 months. The exclusion criteria were occurrence of surgery or recent trauma (less than six months) in the upper or lower limbs; participating in sport at a high (national) level; pregnant or breastfeeding women; occurrence of muscular, neurological, infectious, acute, or chronic inflammatory disease within three weeks of inclusion date; and occurrence of orthopaedic, neuromuscular, or neurological disease with an impact on the quality of the walk.

Demographic data as well as medical and surgical histories were obtained during the baseline visit. A full physical examination, including weight, height, and vital signs, was performed at the first visit and at the 12-month visit. The subjects performed the 6MWT while wearing the sensors at baseline and at 12 months. They also performed the 4SC, rise from floor (RFF), and 10-metre walk test (10MW). All tests were conducted by trained and certified physiotherapists from the neuromuscular centre.

Timed tests

The subjects performed the 6MWT according to the modified ATS guidelines (23). For RFF, trained examiners recorded using a stopwatch the time taken by the patient to complete the task of rising from supine to standing as fast as possible. The test was performed three times with a 1-minute rest between each trial. We kept the best performance. For the 4SC, the subject had to climb a 4-step flight of stairs as fast as possible. The test was performed three times with a 1-minute rest between each trial. We kept the best performance. For the 10-meter walk test, the subject had to walk or run for 10 metres in a straight line. We recorded the time taken to complete the task as fast as possible. The test was performed three times with a 1-minute rest between each trial. We kept the best performance.

Movement monitoring

The ActiMyo® device (Sysnav, Vernon, France) was worn for 1 month at baseline and at 12 months. The two sensors were fixed to the dominant wrist and ankle. According to the EMA, for the purposes of qualification, a recording is considered as valid if it includes at least 50 hours of recording; optimally it should include 180 hours of recording (17). We studied three different variables: stride length, stride velocity, and the number of meters walked per hour. Stride length and stride velocity were studied as the medians (SL50C and SV50C) or the 95th centiles (SL95C or SV95C).

Statistical analysis
Analysis was first performed on the whole sample and then we analysed children (5 to 17 years) and adults (18 years and older) separately. Then within these groups, we analysed male and female subgroups. We used a series of Mann-Whitney U tests to compare subgroups. We then performed correlation analyses using Spearman's rank correlation coefficient based on accelerometer measures, time test performances, age, and height. Finally, we use the Wilcoxon test to assess the evolution of each measure over 12 months. For compliance analysis, we used the 50-h and 180-h thresholds as these two thresholds were defined in the EMA qualification document as acceptable and optimal, respectively (17). All analyses were performed using IBM's SPSS Statistics software. The limit of statistical significance was set to 0.05.

Results

Population

We included 91 healthy individuals (41 males (45.1%) and 50 females (54.9%), with a mean age of 16 years 2 months (15.4) and age ranged between 6 and 85 years. Seven participants withdrew between the baseline and the follow-up visit for personal reasons. A flow chart of subject participation is shown in Fig. 1. The demographic and clinical characteristics of participants whose baseline data were analysed, as well as ActiMyo® variables, are provided in Table 1.

Statistical analysis was performed on data from the 82 participants who achieved more than 50 hours of recording at baseline. For further analysis, healthy subjects were distributed into two age subgroups: those 5 to 17 years of age and those older than 18 years. The first subgroup was composed of 65 participants, 34 of whom were females (52.3%). The second group was composed of 17 participants, of whom 12 were females (70.6%).

The two age groups differed from each other in most measures including height, 6MWD, 4SC, RFF, and stride characteristics (SV50C, SV95C, SL50C and SL95C). Younger subjects were shorter (p < 0.001) but had a higher 6MWD (p = 0.011) than adults. The younger group also performed better at 4SC (p = 0.001) and RFF (p < 0.001). The groups did not differ significantly in 10MW performance (p = 0.079). Regarding magneto-inertial measures, the groups did not differ significantly in the distance walked per hour (p = 0.215). SV50C tended to be higher in the adult group (p = 0.047), whereas SV95C was higher in children (p = 0.001). We found a similar pattern in stride length measures: the median (SL50C) was higher in adults (p = 0.001) but the 95th centile (SL95C) was higher in children (p = 0.001). The ratio between the SV95 and the SV50C was three times higher in younger subjects than in adults, and the ratio between SL95C and SL50C was twice higher in younger subjects, which seems to indicate a more stereotyped walking patterns in adults.

Compliance in wearing the device

Among the 91 healthy controls who wore the wearable device for one month, 90% recorded more than 50 hours, and 77% recorded more than 180 hours at baseline. During the second period, 86% recorded more
than 50 hours, and 73% recorded more than 180 hours. The main reason reported by subjects who recorded less than 50 hours was ‘technical issues’. There was no age or gender effect evident on the recording duration (data not shown).

**Correlations between timed tests, stride parameters and walking activity.**

Table 2 presents correlation coefficients between stride parameters obtained using the wearable device and clinical measures at baseline in both subgroups. We also present data from the 82 subjects who achieved more than 50 hours of recording at baseline. 6MWD was significantly correlated with SV50C, SV95C, and SL95C in the younger group. In the adult group, 6MWD was only correlated with ‘top performance’ measures SV95C and SL95C. In the younger population, the impact of age and height was more obvious than in the adult population (Table 2). Among the group aged 5 to 17 years, height was highly correlated with age, 6MWD, 10MW, SV50C, SL50C, and weakly correlated with SV95C and SL95C. In adults, height was only correlated with stride length measures SL50C and SL95C. We found no correlation between recording duration and stride length, stride velocity, or walking activity (distance/h, p = 0.323; SV50C, p = 0.466; SV95C, p = 0.664; SL50C, p = 0.723 and SL95C, p = 0.798).

**Gender effect**

In the adult population, males showed statistically significantly higher SL50C (p = 0.009) and SL95C (p = 0.001), probably because they are on average taller than women in the cohort (p = 0.048). There was no other difference between males and females in the adult group. In contrast, in the younger population, male subjects were taller than female subjects, but we did not detect significant differences in any qualitative real-life walking parameter between the two subgroups.

**Longitudinal data**

Changes over 12 months are presented in Table 3. We present data on the 73 patients who achieved more than 50 hours of recording both at baseline and on follow-up visits. Given the effects of growth, we investigated two subgroups separately. In the younger group, we observed a significant increase in functional measures (6MWD, 4SC, 10MW) over 1-year. Of the variable instrumented measures, only SL50C increased over 1-year. We did not observe a significant change over 1-year in adults in stride length, stride velocity, distance walked, 6MWD, or RFF with the exception of a slight improvement in the 10MW performance.

**Discussion**

Through this study, we provide normative data for spontaneous stride velocity, stride length and walking distance/hour obtained passively with a wearable device during a 1-month recording period in a non-controlled setting and the 1-year evolution thereafter. The overall compliance with device use was good. More than 90% of subjects wore the device more than the minimum requirement of 50 hours, which indicates that wearing devices at the ankle and at the wrist for 1 month was acceptable for most of
participants. The main reason given for data collection below the 50-hour threshold was ‘technical issues’, and compliance was not influenced by gender or age. In addition, the recording duration did not influence the variables that were studied.

As expected, results of timed tests were growth dependent (22). We also observed the influence of height (in adults) and height and growth (in children) on stride length. These results support previous findings (24, 25). Height did not influence SV95C, for which only a very weak inverse correlation was found with height in the adult subgroup only. In children, all correlations between age, height and stride length or speed were much weaker with top performance as measured by the 95th centile than with median values. Independence of growth is an advantage in clinical trials that are conducted in children over 1 or 2 years, especially in DMD where growth is altered by steroid use.

In comparison with ambulant DMD patients of the same age, healthy children present a 67.3% higher SV95C (17). The difference for other variables was not as extreme, and there is some overlap between DMD and control participants (SL50C 31.39%, SL95C 52.41%, SV50C 25.72%, distance walked/hour 63.13%) (17). SV95C was stable over the one 1-year period in controls but significantly and constantly decreases in subjects with DMD. In DMD patients, there is a significant correlation between SV95C and all timed tests (17). We did not find such correlations in controls, which is probably related to the fact that weakness constitutes a common limiting factor on 6MWD and SV95C in patients with DMD, strengthening the correlation in this group.

Gathering normative data is crucial in the validation process of an outcome measure, as it allows identification of potentially confounding variables such as age, height, or gender. For a specific outcome, the normative data can either show a strong ceiling effect, as is the case for most of normative scales such as CHOP Intend, NSAA, and Motor Function Measure (26–29), or increases with age, as is the case for strength (22, 30) and the 6MWD (21).

The limitation of this study resides in the small number of controls per subgroup (age and gender), principally related to the limited availability of recording devices. Given the number of subjects, we did not study the seasonal influence on the parameters. It is likely that a seasonal analysis would need to take weather conditions into account, as they are more likely to influence walking behaviour than does the time of year, and would require continuous recording over 1-year, which could be burdensome in controls. During the study, participants wore devices on both wrist and ankle. The analysis of upper limb movement in control patients is complex, since there is an interference with movement produced during the ambulation. The results will therefore be presented elsewhere in comparison with the upper limb measures in ambulant and non-ambulant DMD patients.

**Conclusion**

This study provides evidence that normative data regarding stride length and velocity in a home-based environment with wearable sensors is feasible. These normative data will allow us to express a patient’s data as a percentage of predicted value for age or height and to identify those variables that have
important confounding factors. There is still a large amount of work to be done to enable analysis of ambulation and upper limb function in various diseases using medical device for real-life mobility measurement. Future research should focus on exploring new fields of neurological disease and the creation of algorithms to study upper limb function, falls, or ataxia.

**Abbreviations**

4SC: 4-stair climb; 6MWT: 6-minute walk test, 6MWD: 6-minute walk distance; 10MW: 10-metre walk test; DMD: Duchenne Muscular Dystrophy; EMA: European Medicines Agency; NSAA: North Star Ambulatory Assessments; RFF: rise from floor; SV95C: 95th centile stride velocity; SV50C: 50th centile stride velocity; SL95C: 95th centile stride length; SL50C: 50th centile stride length.

**Declarations**

**Acknowledgements**

We would like to thank all of the participants, including parents and guardians, for the time they have provided to this study. We would also like to thank the team at the Citadelle Regional Hospital Centre in Liège, as well as Sysnav in Vernon. We are extremely grateful to the Foundation for Action Duchenne for financial support.

**Funding**

This work was supported by a grant from Action Duchenne.

**Availability of data and materials**

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

**Authors’ contributions**

MP: helped with data analysis and writing the article. AU: experimenter, data collection, data analysis, and writing the article. AD: helped with patient selection, clinical supervision, and data collection. OS, FD, MD: data collection. MA, DE, DV: technical support, data analysis. AD: helped with patient selection, clinical supervision, and data collection. LS: clinical supervision, protocol preparation, and article writing. All authors read and approved the final manuscript.

**Ethics approval and consent to participate**

The study was approved by the ethics committees of the Citadelle Regional Hospital Centre in Liège (Belgian N°: B412201731844), and the experiment was conducted in accordance with the good clinical
practice and with the Declaration of Helsinki (2013). Prior to their inclusion in the study, all participants (and/or their legal guardians) gave their full written informed consent.

**Consent for publication**

Not applicable.

**Competing interests**

Academic authors declare no competing interests. Melanie Anoussamy and Damien Eggenspieler are employed by Synsav, the medium-sized enterprise responsible for ActiMyo® development. David Vissière is the CEO, founder and main shareholder of Sysnav.

**References**

1. Ryder S, Leadley RM, Armstrong N, Westwood M, de Kock S, Butt T, et al. The burden, epidemiology, costs and treatment for Duchenne muscular dystrophy: an evidence review. Orphanet J Rare Dis. 2017;12(1):79.

2. Mah JK, Korngut L, Dykeman J, Day L, Pringsheim T, Jette N. A systematic review and meta-analysis on the epidemiology of Duchenne and Becker muscular dystrophy. Neuromuscul Disord. 2014;24(6):482-91.

3. Bushby K, Finkel R, Wong B, Barohn R, Campbell C, Comi GP, et al. Ataluren treatment of patients with nonsense mutation dystrophinopathy. Muscle Nerve. 2014;50(4):477-87.

4. Mendell JR, Rodino-Klapac LR, Sahenk Z, Roush K, Bird L, Lowes LP, et al. Eteplirsen for the treatment of Duchenne muscular dystrophy. Ann Neurol. 2013;74(5):637-47.

5. Frank DE, Schnell FJ, Akana C, El-Husayni SH, Desjardins CA, Morgan J, et al. Increased dystrophin production with golodirsen in patients with Duchenne muscular dystrophy. Neurology. 2020;94(21):e2270-e82.

6. Aartsma-Rus A, Krieg AM. FDA Approves Eteplirsen for Duchenne Muscular Dystrophy: The Next Chapter in the Eteplirsen Saga. Nucleic Acid Ther. 2017;27(1):1-3.

7. Approval letter for golodirsen. Food and Drug Association. [https://www.accessdata.fda.gov/drugsatfda_docs/nda/2019/211970Orig1s000Approv.pdf](https://www.accessdata.fda.gov/drugsatfda_docs/nda/2019/211970Orig1s000Approv.pdf). Accessed on 1 decembre 2020.

8. Goemans N, Mercuri E, Belousova E, Komaki H, Dubrovsky A, McDonald CM, et al. A randomized placebo-controlled phase 3 trial of an antisense oligonucleotide, drisapersen, in Duchenne muscular dystrophy. Neuromuscul Disord. 2018;28(1):4-15.

9. McDonald CM, Campbell C, Torricelli RE, Finkel RS, Flanagan KM, Goemans N, et al. Ataluren in patients with nonsense mutation Duchenne muscular dystrophy (ACT DMD): a multicentre, randomised, double-blind, placebo-controlled, phase 3 trial. Lancet. 2017;390(10101):1489-98.
10. Voit T, Topaloglu H, Straub V, Muntoni F, Deconinck N, Campion G, et al. Safety and efficacy of drisapersen for the treatment of Duchenne muscular dystrophy (DEMAND II): an exploratory, randomised, placebo-controlled phase 2 study. Lancet Neurol. 2014;13(10):987-96.

11. Assessment report for Kyndrisa. European Medicines Agency. https://www.ema.europa.eu/en/documents/withdrawal-report/withdrawal-assessment-report-kyndrisa_en.pdf. Accessed 1 december 2020.

12. Piwek L, Ellis DA, Andrews S, Joinson A. The Rise of Consumer Health Wearables: Promises and Barriers. PLoS Med. 2016;13(2):e1001953.

13. Dobkin BH. Wearable motion sensors to continuously measure real-world physical activities. Curr Opin Neurol. 2013;26(6):602-8.

14. Caulfield B, Reginatto B, Slevin P. Not all sensors are created equal: a framework for evaluating human performance measurement technologies. NPJ Digit Med. 2019;2:7.

15. Le Moing AG, Seferian AM, Moraux A, Anoussamy M, Dorveaux E, Gasnier E, et al. A Movement Monitor Based on Magneto-Inertial Sensors for Non-Ambulant Patients with Duchenne Muscular Dystrophy: A Pilot Study in Controlled Environment. PLoS One. 2016;11(6):e0156696.

16. Lilien C, Gasnier E, Gidaro T, Seferian A, Grelet M, Vissière D, et al. Home-Based Monitor for Gait and Activity Analysis. J Vis Exp. 2019(150).

17. Qualification opinion on stride velocity 95th centile as a secondary endpoint in Duchenne muscular dystrophy measured by a valid and suitable wearable device*European Medicines Agency. https://www.ema.europa.eu/en/documents/scientific-guideline/qualification-opinion-stride-velocity-95th-centile-secondary-endpoint-duchenne-muscular-dystrophy_en.pdf. Accessed 1 december 2020.

18. Haberkamp M, Moseley J, Athanasiou D, de Andres-Trelles F, Elferink A, Rosa MM, et al. European regulators’ views on a wearable-derived performance measurement of ambulation for Duchenne muscular dystrophy regulatory trials. Neuromuscul Disord. 2019;29(7):514-6.

19. Chabanon A, Seferian AM, Daron A, Péréon Y, Cances C, Vuillerot C, et al. Prospective and longitudinal natural history study of patients with Type 2 and 3 spinal muscular atrophy: Baseline data NatHis-SMA study. PLoS One. 2018;13(7):e0201004.

20. Anoussamy M, Seferian AM, Daron A, Péréon Y, Cances C, Vuillerot C, et al. Natural history of Type 2 and 3 spinal muscular atrophy: 2-year NatHis-SMA study. Ann Clin Transl Neurol. 2020.

21. Goemans N, Klingels K, van den Hauwe M, Boons S, Verstraete L, Peeters C, et al. Six-minute walk test: reference values and prediction equation in healthy boys aged 5 to 12 years. PLoS One. 2013;8(12):e84120.

22. Hogrel JY, Decostre V, Ledoux I, de Antonio M, Niks EH, de Groot I, et al. Normalized grip strength is a sensitive outcome measure through all stages of Duchenne muscular dystrophy. J Neurol. 2020;267(7):2022-8.

23. McDonald CM, Henricson EK, Han JJ, Abresch RT, Nicorici A, Elfring GL, et al. The 6-minute walk test as a new outcome measure in Duchenne muscular dystrophy. Muscle Nerve. 2010;41(4):500-10.
24. Dusing SC, Thorpe DE. A normative sample of temporal and spatial gait parameters in children using the GAITRite electronic walkway. Gait Posture. 2007;25(1):135-9.

25. Pierrynowski MR, Galea V. Enhancing the ability of gait analyses to differentiate between groups: scaling gait data to body size. Gait Posture. 2001;13(3):193-201.

26. Clinical Review Report: Nusinersen (Spinraza): (Biogen Canada Inc.): Indication: Treatment of patients with 5q SMA [Internet]. Ottawa (ON): Canadian Agency for Drugs and Technologies in Health; 2018 Jan. https://www.ncbi.nlm.nih.gov/books/NBK533989/. Accessed 1 december 2020.

27. de Lattre C, Payan C, Vuillerot C, Rippert P, de Castro D, Bérard C, et al. Motor function measure: validation of a short form for young children with neuromuscular diseases. Arch Phys Med Rehabil. 2013;94(11):2218-26.

28. Klingels K, Van Verdegem L, van den Hauwe M, Buyse G, Goemans N. Reference values for the three-minute walk test, North Star ambulatory assessment and timed tests in typically developing boys aged 2.5-5 years. Neuromuscular Disorders. 2015;25:S228.

29. Kolb SJ, Coffey CS, Yankey JW, Krosschell K, Arnold WD, Rutkove SB, et al. Baseline results of the NeuroNEXT spinal muscular atrophy infant biomarker study. Ann Clin Transl Neurol. 2016;3(2):132-45.

30. Servais L, Deconinck N, Moraux A, Benali M, Canal A, Van Parys F, et al. Innovative methods to assess upper limb strength and function in non-ambulant Duchenne patients. Neuromuscul Disord. 2013;23(2):139-48.

Tables

Table 1. Demographic and clinical characteristics of participants who recorded more than 50 hours.

| Measure                      | Description                        | Data Type |
|------------------------------|------------------------------------|-----------|
| 6MWT                         | 6-minute walk distance              | Mean (SD) |
| 4SC                          | 4-stair climb                       |           |
| RFF                          | rise from floor                     |           |
| 10MW                         | 10-metre walk test                  |           |
| SV50C                        | 50th centile stride velocity        |           |
| SV95C                        | 95th centile stride velocity        |           |
| SL50C                        | 50th centile stride length          |           |
| SL95C                        | 95th centile stride length          |           |

6MWT: 6-minute walk distance, 4SC: 4-stair climb; RFF: rise from floor; 10MW: 10-metre walk test; SV50C: 50th centile stride velocity; SV95C: 95th centile stride velocity; SL50C: 50th centile stride length; SL95C: 95th centile stride length. Data are expressed in mean (SD) [Min-Max]
| Characteristics       | Children | Adult | All    |
|-----------------------|----------|-------|--------|
| Sample size           | 65       | 17    | 82     |
| Age (years)           | 10.1 (2.8) | 43 (18.9) | 15.9 (16.0) |
|                       | [6.0 – 17.6] | [18.0 – 84.3] | [6.0 – 84.3] |
| Height (cm)           | 137.8 (14.5) | 167.5 (10.6) | 144.0 (18.3) |
|                       | [114.0 – 173.3] | [153.2 – 195.0] | [114.0 – 195.0] |
| 6MWT (m)              | 606.0 (64.1) | 551.5 (82.0) | 594.7 (71.2) |
|                       | [464.0 – 761.0] | [436.0 – 716.0] | [435.0 – 761.0] |
| Four stairs climb (s) | 1.3 (0.3) | 1.6 (0.4) | 1.4 (0.3) |
|                       | [0.9 – 2.3] | [1.1 – 2.3] | [0.9 – 2.3] |
| Rise From floor (s)   | 1.6 (0.2) | 2.7 (0.9) | 1.8 (0.6) |
|                       | [1.0 – 2.2] | [1.2 – 4.9] | [1.0 – 4.9] |
| 10MW (m)              | 4.7 (0.7) | 5.1 (0.8) | 4.8 (0.8) |
|                       | [3.1 – 7.2] | [4.1 – 7.3] | [3.1 – 7.3] |
| Distance/hour (m/h)   | 270.2 (86.5) | 246.4 (89.5) | 265.2 (87.2) |
|                       | [39.9 – 484.4] | [119.6 – 433.0] | [39.9 – 484.4] |
| SV50C (m/s)           | 1.0 (0.1) | 1.1 (0.1) | 1.0 (0.1) |
|                       | [0.9 – 1.3] | [0.7 – 1.3] | [0.7 – 1.3] |
| SV95C (m/s)           | 2.6 (0.4) | 1.6 (0.3) | 2.4 (0.6) |
|                       | [1.6 – 3.6] | [1.1 – 2.3] | [1.1 – 3.6] |
| SL50C (m)             | 1.0 (0.1) | 1.2 (0.1) | 1.1 (0.1) |
|                       | [0.8 – 1.4] | [0.8 – 1.5] | [0.8 – 1.5] |
| SL95C (m)             | 1.7 (0.2) | 1.5 (0.2) | 1.7 (0.2) |
|                       | [1.4 – 2.3] | [1.1 – 1.8] | [1.1 – 2.3] |

Table 2 Correlation between accelerometer measures and clinical measures (Spearman coefficient). Significance level $p \leq 0.01**$, $p \leq 0.05*$. Lower part: correlation on the whole sample. Upper part: correlation on the two age groups. 6MWT: 6-minute walk distance, 4SC: 4-stair climb; RFF: rise from floor; 10MW: 10-metre walk test; SV50C: 50th centile stride velocity; SV95C: 95th centile stride velocity; SL50C: 50th centile stride length; SL95: 95th centile.
Table 3. Evolution of measures over 12 months. Time effect was assessed by a rank Wilcoxon test for single sample (null hypothesis: median=0). Significance level $p \leq 0.01^{**}$, $p \leq 0.05^{*}$. 6MWT: 6-minute walk distance, 4SC: 4-stair climb; RFF: rise from floor; 10MW: 10-metre walk test; SV50C: 50th centile stride velocity; SV95C: 95th centile stride velocity; SL50C: 50th centile stride length; SL95C: 95th centile stride length.
| Characteristics   | 5-17 years old |   | Over 18 years old |   |
|-------------------|---------------|---|-------------------|---|
|                   | Mean (SD)     | Sig. | Mean (SD)        | Sig. |
| Δ6MWD (m)         | 33.6 (50.302) | \( p = 0.000^{**} \) | 14.87 (46.649) | \( p = 0.191 \) |
| Δ4SC (s)          | -0.11 (0.288) | \( p = 0.004^{**} \) | -0.02 (0.463)  | \( p = 0.875 \) |
| ΔRFF (s)          | -0.07 (0.336) | \( p = 0.293 \)    | -0.24 (0.736)  | \( p = 0.239 \) |
| Δ10MW (s)         | -0.76 (0.77)  | \( p = 0.000^{**} \) | -0.52 (0.632)  | \( p = 0.011^{*} \) |
| ΔDistance (m/h)   | -17.23 (76.17)| \( p = 0.059 \)    | 9.38 (67.15)   | \( p = 0.609 \) |
| ΔSV50C (m/s)      | 0.01 (0.078)  | \( p = 0.359 \)    | 0.01 (0.154)   | \( p = 0.691 \) |
| ΔSV95C (m/s)      | -0.12 (0.447) | \( p = 0.112 \)    | 0.12 (0.389)   | \( p = 0.955 \) |
| ΔSL50C (m)        | 0.05 (0.06)   | \( p = 0.000^{**} \) | 0.01 (0.095)   | \( p = 0.427 \) |
| ΔSL95C (m)        | 0.02 (0.184)  | \( p = 0.241 \)    | 0.04 (0.133)   | \( p = 0.691 \) |

**Figures**
Figure 1

Flow-chart displaying the compliance and inclusion of subjects. Withdrawals resulted from loss of follow up (5 subjects) and withdrawal by the subject (2 subjects).