Gray matter structural covariance networks changes along the Alzheimer's disease continuum

Kaicheng Li, Xiao Luo, Qingze Zeng, Peiyu Huang, Zhujing Shen, Xiaojun Xu, Jingjing Xu, Chao Wang, Jiong Zhou, Minming Zhang, for the Alzheimer's Disease Neuroimaging Initiative

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ABSTRACT
Alzheimer's disease (AD) has a long neuropathological accumulation phase before the onset of dementia. Such AD neuropathological deposition between neurons impairs the synaptic communication, resulting in networks disorganization. Our study aimed to explore the evolution patterns of gray matter structural covariance networks (SCNs) along AD continuum. Based on the AT(N) (i.e., Amyloid/Tau/Neurodegeneration) pathological classification system, we classified subjects into four groups using cerebrospinal fluid amyloid-beta1–42 (A) and phosphorylated tau protein181 (T). We identified 101 subjects with normal AD biomarkers (A-T-), 40 subjects with Alzheimer's pathologic change (A+T−), 101 subjects with biological AD (A+T+) and 91 AD with dementia (demented subjects with A+T+). We used four regions of interest to anchor default mode network (DMN, medial temporal subsystem and midline core subsystem), salience network (SN) and executive control network (ECN). Finally, we used a multi-regression model-based linear-interaction analysis to assess the SCN changes. Along the disease progression, DMN and SN showed increased structural association at the early stage while decreased structural association at the late stage. Moreover, ECN showed progressively increased structural association as AD neuropathological profiles progress. In conclusion, this study found the dynamic trajectory of SCNs changes along the AD continuum and support the network disconnection hypothesis underlying AD neuropathological progression. Further, SCN may potentially serve as an effective AD biomarker.

1. Introduction
Alzheimer's disease (AD) is the most common form of dementia, which was characterized clinically by progressive memory and other cognitive abilities decline. At the neuropathological level, AD neuropathological accumulation begins years before the onset of dementia (Villemagne et al., 2013) and develops in a specific temporal-ordered manner (Sperling et al., 2014), with extracellular amyloid-β plaques deposit appears the earliest and followed by intracellular phosphorylated tau protein deposition and downstream neurodegeneration events (Jack Jr. et al., 2013). Hence, combining the pathological stages with the symptomatic diagnosis can help to assess AD continuum more accurately (Montal et al., 2018).

Spatially, AD neuropathological deposition around neurons impairs synaptic communication, resulting in neuronal networks disorganization (Myers et al., 2014). As such, AD is regarded as a disconnection disease featuring intrinsic network disorganization (Delbeuck et al., 2003). The most commonly affected brain regions in AD studies are the default mode network (DMN), salience network (SN) and executive control network (ECN), which cooperate to maintain cognitive abilities including memory, and executive function (Zhu et al., 2016; Seeley et al., 2007). Notably, recent studies also reported that the DMN consists of multiple, spatially dissociated but interactive subsystems, including the midline core subsystem (self-relevant decision-making) and medial temporal subsystem (episodic memory) (Andrews-Hanna et al., 2010; Uddin et al., 2009). Moreover, these network disruptions have
been associated with cognitive dysfunction in AD. Therefore, brain network analysis could be an effective method to study AD neuropathology and explore further cognitive changes.

Brain networks can be constructed based on similarity in GM structure between brain areas, which was named as the gray matter (GM) structural covariance network (SCN) (Mechelli et al., 2005; Alexander-Bloch et al., 2013a; Tijms et al., 2012). Based on prior studies, the biological meaning of SCN may link to coordinated GM growth during development (Alexander-Bloch et al., 2013a), functional co-activation (Alexander-Bloch et al., 2013b), axonal connectivity (Essen, 1997; Gong et al., 2012a) and genetic factors (Chen et al., 2013; Schmitt et al., 2009; Alexander et al., 2012). Brain areas that are highly correlated in size are always part of systems that subserving specific behavioral or cognitive functions (Alexander-Bloch et al., 2013a; Zielinski et al., 2010). For example, areas involved in memory showed GM volume covariance (Bobbot et al., 2007). In AD, SCN showed disorganization which correlates with cognitive dysfunction (Dicks et al., 2018; Tijms BM Kate et al., 2016). Specifically, Spreng et al. demonstrated decreased SCN in DMN in AD patients (Spreng and Turner, 2013). Another SCN study showed that early AD patients had decreased structural association within the DMN while increased structural association in the SN and ECN (Montembeault et al., 2016). These results indicate the trend of decreased structural association in DMN while increased structural association in ECN and SN in AD patients. However, few studies considered the AD neuropathological stages. This may lead to inaccurate results considering the temporal-ordered neuropathological propagation along the network.

To address this gap, the current study aimed to explore the trajectory of SCN changes along the pathophysiological continuum of AD. Combining the neuropathological hallmarks and symptomatic status, we classified the subjects into four groups to reflect the disease progression along the AD continuum. According to the evidence that AD network highly linked to its neuropathological state (Seeley et al., 2009; Knobloch and Mansuy, 2008), we hypothesized that DMN tends to show a decreased structural association while the ECN and SN tend to show an increased structural association as AD progresses.

2. Methods and materials

2.1. Alzheimer's disease neuroimaging and initiative

Data used in the preparation of this article were obtained from the Alzheimer’s disease Neuroimaging Initiative (ADNI) database (http://adni.loni.usc.edu). The ADNI was initially launched in 2004 (ADNI-1), and additional recruitment was made through ADNI-GO in 2009, ADNI-2 in 2010 and ADNI-3 in 2016. The primary goal of ADNI has been to identify serial MRI, PET, biomarkers and genetic characteristics that would support the early detection and tracking of the AD, and improved clinical trial design. For up-to-date information, see http://www.adni-info.org.

2.2. Study participants

This study was approved by the Institutional Review Boards of all participating institutions and informed written consent was obtained from all participants at each site. Similar to the previous study (Palmqvist et al., 2017), we identified 242 non-demented subjects (characterized as either cognitively unimpaired or mild cognitive impairment, MCI) and 91 demented subjects from ADNI database (Table 1, the flowchart in Supplementary Material 1). We included MCI subjects since the cognitive impairment may be not caused by an underlying AD process and, given that about a third of MCI were incorrectly diagnosed (Bangen KJ Clark et al., 2016; Edmonds EC Delano-Wood L, Galasko DR, Salmon DP, Bondi MW1; Alzheimer's Disease Neuroimaging Initiative, 2014). Furthermore, based on the pathological system (Jack et al., 2018), we identified demented subjects in the study since the Alzheimer’s disease with dementia features the highest risk of clinical progression and can present the most classic AD-related changes.

Cognitively unimpaired subject was defined as having a Clinical Dementia Rating scale (CDR) score of 0, an Mini-Mental State Examination (MMSE) between 24 and 30 (inclusive), a normal Wechsler Memory Scale Logical Memory, WMS-LM, delay recall performance (in detail: ≥ 9 for subjects with 16 or more years of education; ≥ 5 for subjects with 8–15 years of education; and ≥ 3 for 0–7 years of education); absence of clinical depression (geriatric depression scale-15, GDS-15 score < 6) (Sheikh and Yesavage, 1986) and absence of dementia. MCI (Bondi et al., 2014) was defined as having preserved activities of daily living, the absence of dementia, and objective cognitive impairment as shown on the delayed recall test of the WMS-LM as well as a CDR score of 0.5. Demented individuals were defined as having an MMSE score of ≤26, and a clinical dementia rating (CDR) of ≥0.5 as well as satisfying the NINCDS/ADRDA criteria for probable AD (McKhann et al., 1984). We excluded subjects with the following manifestations: (a) significant medical, neurological, and psychiatric illness; (b) obvious head trauma history; (c) use of non-AD-related medication known to influence cerebral function; (d) clinical depression; (e) alcohol or drug abuse. Only subjects with a simultaneous structural scan, lumbar puncture, and comprehensive neuropsychological assessments were included.

2.3. Neuropsychological assessment and CSF data acquisition

All subjects underwent comprehensive neuropsychological tests (Table 1, description about demographics in Supplementary Material 2), including assessment of general mental status (Mini-Mental State Examination, MMSE; Clinical Dementia Rating, CDR) and other cognitive domains, involving memory function (Auditory Verbal Learning Test, AVLT; WMS-LM, immediate and delayed memory), attention (Trail-Making Test part A, TMT-A), visuospatial function (Clock- Drawing Test, CDT), decision-making function (Trail-Making Test part B, TMT-B), and language ability (Boston Naming Test, BNT; Category fluency).

CSF biomarkers comprise amyloid-beta1–42 (Aβ1–42), total tau (T-tau), and phosphorylated tau at position181 (P-tau181), measured by the multiplex xMAP Luminex platform as previously described (Shaw et al., 2009) (Table 1).

2.4. Group classifications

We combined the latest pathological classification model (Jack et al., 2018) with the symptomatic diagnosis to reflect the disease progression along the AD continuum. Specifically, this model uses three major neuropathological biomarkers: amyloid deposition (A), pathologic tau (T), and neurodegeneration (N) [AT(N)] to stage the disease pathology across entire AD continuum in vivo (Supplementary Material 3). As previous studies described, we set the CSF cutoff point at 192 pg/ml for Aβ1–42 and 23 pg/ml for P-tau181 (Shaw et al., 2009; Meyer et al., 2010). Subsequently, based on the pathological AT(N) system, we classified all subjects into four groups according to their CSF Aβ1–42 and P-tau181 level: (a) Group 0: subjects with normal AD biomarkers, consisting of non-demented individuals with normal Aβ1–42 and P-tau181 (A − T −); (b) Group 1: subjects with Alzheimer’s pathologic change, consisting of non-demented individuals with abnormal Aβ1–42 and normal P-tau181 (A + T −); (c) Group 2: subjects with biological Alzheimer’s disease, consisting of demented individuals with abnormal Aβ1–42 and normal P-tau181 (A + T +); (d) Group 3: Alzheimer’s disease with dementia, consisting of demented subjects with abnormal Aβ1–42 and P-tau181 (A + T +). Notably, we excluded subjects with normal Aβ1–42 and abnormal P-tau181 (A-T +) since it was considered as a non-AD related pathology (Jack Jr. et al., 2016).
Table 1
Demographic and neuropsychological data in subjects along the AD continuum.

| Demographic characteristics | Group 0 \(N = 101\) | Group 1 \(N = 40\) | Group 2 \(N = 101\) | Group 3 \(N = 91\) | P-value |
|-----------------------------|---------------------|---------------------|---------------------|---------------------|---------|
| Age, y, mean (SD)           | 71.40 ± 6.29        | 72.70 ± 7.01        | 72.68 ± 5.70        | 73.34 ± 7.76        | G1-G0 = 0.29, G2-G0 = 0.13, G3-G0 = 0.06 |
| Female, n(%)                | 51(50.50%)          | 14(35.00%)          | 45(44.55%)          | 41(45.05%)          | G1-G0 = 0.07, G2-G0 = 0.24, G3-G0 = 0.27 |
| Education, y, mean (SD)     | 16.42 ± 2.66        | 16.38 ± 2.61        | 16.36 ± 2.40        | 15.80 ± 2.45        | G1-G0 = 0.93, G2-G0 = 0.87, G3-G0 = 0.10 |
| APOE ε4 status, n(%)        | 16(15.84%)          | 15(37.50%)          | 61(60.39%)          | 67(73.63%)          | G1-G0 < 0.001, G2-G0 < 0.001, G3-G0 < 0.001, G4-G0 < 0.001 |
| GDS                          | 1.30 ± 1.42         | 1.43 ± 1.55         | 1.50 ± 1.59         | 1.64 ± 1.38         | G1-G0 = 0.64, G2-G0 = 0.35, G3-G0 = 0.09 |
| General mental status       |                    |                     |                     |                     |         |
| MMSE                         | 28.77 ± 1.38        | 28.80 ± 1.27        | 28.17 ± 1.73        | 23.00 ± 2.30        | G1-G0 = 0.91, G2-G0 = 0.40, G3-G0 < 0.001, G4-G0 < 0.001 |
| CDR global                   | 0.30 ± 0.25         | 0.26 ± 0.25         | 0.36 ± 0.22         | 0.80 ± 0.28         | G1-G0 = 0.40, G2-G0 = 0.08, G3-G0 < 0.001, G4-G0 < 0.001 |
| CDR sum                      | 0.79 ± 0.82         | 0.73 ± 0.91         | 1.18 ± 1.11         | 4.63 ± 1.80         | G1-G0 = 0.71, G2-G0 = 0.01, G3-G0 < 0.001, G4-G0 < 0.001 |
| Memory function              |                    |                     |                     |                     |         |
| WMS-LM immediate             | 12.76 ± 3.20        | 13.18 ± 3.37        | 11.04 ± 4.21        | 3.93 ± 2.49         | G1-G0 = 0.53, G2-G0 = 0.001, G3-G0 < 0.001, G4-G0 < 0.001 |
| WMS-LM delay                 | 10.87 ± 3.44        | 11.65 ± 3.76        | 9.04 ± 4.64         | 1.47 ± 1.70         | G1-G0 = 0.24, G2-G0 = 0.002, G3-G0 < 0.001, G4-G0 < 0.001 |
| AVLT sum of trials 1–5       | 44.71 ± 11.64       | 41.75 ± 11.08       | 37.28 ± 10.63       | 21.96 ± 7.42        | G1-G0 = 0.169, G2-G0 < 0.001, G3-G0 < 0.001, G4-G0 < 0.001 |
| AVLT 30 min                  | 7.19 ± 4.04         | 6.60 ± 3.80         | 4.33 ± 3.92         | 0.51 ± 1.07         | G1-G0 = 0.43, G2-G0 < 0.001, G3-G0 < 0.001, G4-G0 < 0.001 |
| Attention                    |                    |                     |                     |                     |         |
| Log-transformed TMT-A        | 1.51 ± 0.14         | 1.54 ± 0.16         | 1.55 ± 0.14         | 1.71 ± 0.21         | G1-G0 = 0.34, G2-G0 = 0.08, G3-G0 < 0.001, G4-G0 < 0.001 |
| Decision-making function     |                    |                     |                     |                     |         |
| Log-transformed TMT-B        | 1.90 ± 0.18         | 1.94 ± 0.19         | 1.95 ± 0.20         | 2.23 ± 0.21         | G1-G0 = 0.27, G2-G0 = 0.08, G3-G0 < 0.001, G4-G0 < 0.001 |
| Language                     |                    |                     |                     |                     |         |
| BNT total                    | 27.71 ± 2.62        | 27.68 ± 2.26        | 27.73 ± 2.96        | 21.67 ± 6.00        | G1-G0 = 0.93, G2-G0 = 0.96, G3-G0 < 0.001, G4-G0 < 0.001 |
| Category fluency             | 19.59 ± 5.10        | 18.35 ± 5.83        | 19.26 ± 5.36        | 11.70 ± 4.89        | G1-G0 = 0.22, G2-G0 = 0.65, G3-G0 < 0.001, G4-G0 < 0.001 |
| Visuospatial processing      | 4.59 ± 0.67         | 4.43 ± 0.71         | 4.57 ± 0.35         | 3.49 ± 1.45         | G1-G0 = 0.19, G2-G0 = 0.84, G3-G0 < 0.001, G4-G0 < 0.001 |
| CSF Aβ1-42 (pg/ml)           | 228.93 ± 23.66      | 159.92 ± 26.80      | 136.75 ± 25.24      | 126.71 ± 20.74      | G1-G0 < 0.001, G2-G0 < 0.001, G3-G0 < 0.001, G4-G0 < 0.001 |

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2.5. MRI acquisition and pre-processing

MRI data were acquired in 3T scanners. Briefly, the ADNI protocol includes T1-weighted acquisition based on a sagittal volumetric magnetization-prepared rapid gradient echo sequence collected from a variety of MR systems with protocols optimized for each type of scanner. Representative imaging parameters were as follows: repetition time (TR) = 2300 ms; echo time (TE) = 3 ms; within plane FOV = 256 × 256 mm²; voxel size = 1.1 × 1.1 × 1.2 mm³; flip angle = 9° or 11°.

We pre-processed all T1-weighted images using the Computational Anatomy Toolbox (CAT12, http://dbm.neuro.uni-jena.de/cat12/) toolbox segment data pipeline implemented within SPM12 in Matlab (R2012b). First, the T1 image was spatially registered to the tissue probability maps (TPM) and then segmented into gray matter (GM), white matter (WM) and cerebrospinal fluid (CSF). We performed the affine registration to the stereotactic MNI space using ICBM152 space. Second, we performed high-dimensional DARTEL normalization and nonlinear modulation using the Jacobian determinants derived from the normalization process. To remove the MRI inhomogeneities and noise, we corrected the bias, noise and normalized the intensities. Subsequently, we smoothed the GM image with a Gaussian kernel of 8 × 8 × 8 mm³ to reduce potential inaccuracies during the normalization step. Moreover, we assessed processed image quality by visual inspection and weighted average image quality index (using the quality assurance (QA) framework in CAT 12, http://www.neuro.uni-jena.de/cat/). Here, we only include the subjects with QA better than C+.

Finally, 64 subjects did not pass the image quality control.

2.6. Structural covariance gray matter network

To construct the SCNs, we chose four regions of interest (ROIs) (Montembeault et al., 2016): right entorhinal cortex (EC, MNI coordinates: 25, −9, −28) (Bernhardt et al., 2008; Eickhoff et al., 2005), left posterior cingulate cortex (PCC, MNI coordinates: −2, −36, 35) (Spreng and Turner, 2013; Zieminski et al., 2012), right frontoinsular cortex (FIC, MNI coordinates: 38, 26, −10), and right dorsolateral prefrontal cortex (DLPFC, MNI coordinates: 44, 36, 20) (Zieminski et al., 2010; Montembeault et al., 2016). These regions anchor the default mode network (DMN, medial temporal subsystem), DMN (midline core subsystem), salience network (SN) and executive control network (ECN) respectively.

To achieve SCN t-maps, we performed the general linear analysis on modulated GM images. Specifically, we extracted the GM volume from a 4-mm radius sphere (Montembeault et al., 2016; Chang et al., 2018; Chang et al., 2017) around those coordinates on modulated images. Then, we performed four separate correlation analysis by entering the GM volumes of each ROI as a regressor and the total intracranial volume, gender, age, and education as covariates. Before statistical correction, we performed Fisher’s Z transformation. For each group, we performed specific contrasts to identify voxels expressing a positive correlation with each ROI. We set the threshold at P ≤ 0.01 corrected for false discovery rate (FDR). Considering the physiological meanings of the SCN clusters, we reported clusters showing cluster size > 10 voxels (Chang et al., 2018; Chang et al., 2017). To achieve qualitative group-wise comparisons, we displayed the results on a standard brain template (ICBM152).

Then, we used multi-regression model-based linear interaction analysis (Bernhardt et al., 2008) to assess how the disease stage interferes with SCN, voxels showing significant differences in the regression slopes in each ROI were compared. For this study, we refer to these differences in slopes as the differences in “structural association”. We set the threshold at p < 0.05 at voxel level, p < 0.05 at cluster level, with Gaussian random field correction (GRF) corrected.

To explore the clinical significance of the identified peak voxel volume, we performed the correlation analysis (Chang et al., 2018; Chang et al., 2017). To be specific, for the peak clusters showing significant between-group differences, we extracted the GM volume using a 4-mm radius sphere placing on the peak voxel. Then, we conducted Pearson correlation analysis between the peak voxel volume and neuropsychological data within each group which showed the difference in the structural association. The threshold was set at p < 0.05, Bonferroni corrected.

3. Results

3.1. Patterns of structural association within each group

To qualitatively compare the patterns of positive correlations in subjects at all groups, we presented the statistical maps in Fig. 1. Regions presenting a structural association with the seed regions of each network in each group are listed in supplementary material 4.

In both DMN midline core subsystem and ECN, the subjects in Group 3 presents a greater extent of structural covariance than Group 0; In both DMN medial temporal subsystem and SN, the subjects in Group 3 presents a decreased extent of structural covariance than Group 0.

3.2. VThe difference of structural covariance gray matter network

Regarding DMN medial temporal subsystem, subjects in Group 2 showed an increased structural association between the EC and middle temporal gyrus (MTG); subjects in Group 3 showed a decreased structural association between the EC and MTG as well as superior frontal gyrus (SFG) compared to subjects in Group 0. Regarding the DMN midline core subsystem, no significant difference existed in Group 1, 2, or 3 compared to Group 0. Regarding SN, subjects in Group 1 showed
an increased structural association between FIC and precuneus; as pathological accumulation progressed, subjects in Group 3 showed the decreased structural association between FIC and the inferior temporal gyrus. Regarding ECN, subjects in Group 1 and Group 3 showed an increased structural association between DLPFC and SFG (Fig. 2 and Table 2). Moreover, to qualitatively depict the SCNs pattern, we also performed the group difference analysis between Group 1, 2, and 3 (Supplementary Material 8).

Additionally, we performed an analysis using the contralateral ROI seeds by changing the sign on each seed’s x coordinate (Zielinski et al., 2010). DMN showed initially increased and then decreased structural association between EC and frontal region along AD continuum. SN showed the increased structural association between FIC and inferior parietal gyrus at the early neuropathological stage (Supplementary Material 5).

To test the reliability, we adopted different statistical thresholds. Results remained mostly unchanged (Supplementary Material 6). Moreover, we repeated the analysis based on ADNI1 database (acquired from 1.5 T MRI scanner). Similarly, DMN showed a trend of the decreased structural association while ECN showed a trend of increased structural association (Supplementary Material 7).

### 3.3. Correlations of peak cluster volumes with neuropsychological scores

We then performed the Pearson correlation analysis between the peak cluster volumes and neuropsychological scores. The correlation mainly located at the EC anchored DMN medial temporal subsystem, concerning memory and language (Table 3). To be specific, in Group 3 subjects, the peak volume of MTG significantly correlated with memory (WMS-LM immediate and delay \( r = 0.34, p < 0.005, r = 0.30, p < 0.005 \), respectively); AVLT sum of trials 1–5 \( r = 0.34, p < 0.005 \)), language (category fluency \( r = 0.42, p < 0.001 \)), BNT total \( r = 0.39, p < 0.001 \)), and executive function (log-transformed TMT-B \( r = -0.33, p < 0.005 \)). Moreover, regarding DLPFC anchored ECN, in Group 3 subjects, the peak volume of SFG negatively correlated with log-transformed TMT-A \( r = -0.48, p < 0.001 \) and log-transformed TMT-B \( r = -0.48, p < 0.001 \).

### 4. Discussion

Our study explored the SCN changes along the AD continuum based on the neuropathological classification system. Regarding the DMN and...
Fig. 2. The difference of Gray Matter Structural Covariance network between subjects in AD continuum and Group 0.

(A) As for DMN medial temporal subsystem, subjects in Group 2 showed an increased structural association between the EC and MTG; subjects in Group 3 showed a decreased structural association between the EC and MTG as well as SFG when compared to subjects in Group 0. (B) As for SN, subjects in Group 1 showed an increased structural association between FIC and precuneus; subjects in Group 3 showed decreased association between FIC and the inferior temporal gyrus. (C) As for ECN, subjects in Group 1 in Group 3 showed an increased structural association in the SFG.

Abbreviations: DMN: default mode network; SN: salience network; ECN: executive control network; EC: entorhinal cortex; FIC: frontoinsular cortex; DLPFC: dorsolateral prefrontal cortex; MTG: middle temporal gyrus; SFG: superior frontal gyrus; Group 0: subjects with normal AD biomarkers, non-demented individuals without abnormal CSF; Group 1: subjects with Alzheimer’s pathologic change, non-demented individuals with abnormal Aβ1–42 but normal P-tau181; Group 2: subjects with biological Alzheimer’s disease, non-demented individuals with abnormal Aβ1–42 and P-tau181; Group 3: Alzheimer’s disease with dementia, demented individuals with abnormal Aβ1–42 and P-tau181.

Table 2

The difference of gray matter structural covariance network between subjects in AD continuum and Group 0.

| Network                    | Group                  | Peak region              | MNI coordinates | Extent | Peak intensity |
|----------------------------|------------------------|--------------------------|-----------------|--------|----------------|
| Default mode (medial temporal lobe subsystem) (R EC) | Group 2 VS. Group 0 | L. Middle Temporal Gyrus | −49.5 −19.5 −4.5 | 8811   | 4.81           |
|                            | Group 3 VS. Group 0   | L. Middle Temporal Gyrus | −45 4.5 −31.5   | 9380   | −4.25          |
|                            |                        | L Superior Frontal Gyrus | 12 36 36        | 6031   | −3.80          |
| Salience (R FIC)           | Group 1 VS. Group 0   | L. Precuneus             | −12 −58.5 36    | 3992   | 3.80           |
|                            | Group 3 VS. Group 0   | L. Inferior Temporal Gyrus | −55.5 −33 −22.5 | 4167   | −4.24          |
| Executive Control (R DLPFC)| Group 1 VS. Group 0   | R. Superior Frontal Gyrus | 12 27 36        | 3208   | 3.85           |
|                            | Group 3 VS. Group 0   | R. Superior Frontal Gyrus | 18 6 55.5       | 9977   | 4.50           |

Abbreviation: R: right; EC: entorhinal cortex; FIC: frontoinsular cortex; DLPFC: dorsolateral prefrontal cortex; Group 0: subjects with normal AD biomarkers, non-demented individuals without abnormal CSF; Group 1: subjects with Alzheimer's pathologic change, non-demented individuals with abnormal Aβ1–42 but normal P-tau181; Group 2: subjects with biological Alzheimer's disease, non-demented individuals with abnormal Aβ1–42 and P-tau181; Group 3: Alzheimer's disease with dementia, demented individuals with abnormal Aβ1–42 and P-tau181.
The DMN, SN (Suppekar et al., 2008; Zhou et al., 2010) and the pathological progression provide support for the disconnection hypothesis underlying AD neuropathological profiles progress. Our results suggest the dy abnormal CSF showed progressively increased structural association as subjects at the early and late stage of AD successively showed in-pathologic change, non-demented individuals with abnormal Aβ1–42 but normal P-tau181; Group 2: G2, subjects with biological Alzheimer's disease, non-demented individuals with abnormal Aβ1–42 and P-tau181; Group 3: G3, Alzheimer’s disease with dementia, demented individuals with abnormal Aβ1–42 and P-tau181.

Abbreviation: EC: entorhinal cortex; DLPFC: dorsolateral prefrontal cortex; FIC: frontoinsular cortex; MTG: middle temporal gyrus; SFG: superior frontal gyrus; ITG: inferior temporal gyrus; CDT: Clock Drawing Test.

These results are partially in line with previous studies which reported first increased (between CDR 0 and CDR 0.5) and then decreased structural association in ITG in Group 3 subjects. These results are in line with one functional study, which showed the trend of an increased structural association involving the temporal and frontal regions. These changes could be described as a biphasic trajectory which was resulted by neuropathological progression. Moreover, such DMN changes always correlate with cognitive status and CSF level (Spreng and Turner, 2013; Allen et al., 2007; Zhang et al., 2010). One SCN study found a decreased association between EC and MTG in Group 2 and decreased structural association between EC and MTG as well as SFG in Group 3.

Although SCN could not be considered as a direct measure of connectivity, convergent studies reported the spatial overlap between intrinsic connectivity and structural covariance, thus demonstrating that these patterns mirror each other (Mechelli et al., 2005; Seeley et al., 2009; Segal et al., 2012; Zhang et al., 2011; Lerch et al., 2006). This could be explained by the fact that synchronous neuronal firing promotes network based synaptogenesis (Katz and Shatz, 1996; Bi and Poo, 1999). Accordingly, GM SCN could indicate the connectivity to some extent and provide additional insight into the network topographical organization (Alexander-Bloch et al., 2013a; Bassett and Bullmore, 2009; Gong et al., 2012b). Here, decreased correlations between brain regions may be suggestive of disconnectivity or localization degeneration while increased correlations may indicate overconnectivity or correlated gray matter loss in regions targeted by the same neurodegenerative process.

Regarding the DMN, subjects at the early and late stage of AD showed increased structural association while decreased association in subjects at the late stage. This result is in line with previous studies which reported the early involvement of DMN in AD (Seeley et al., 2009; He et al., 2007; Luo et al., 2018a; Luo et al., 2018b; Gili et al., 2011), and the progressive SCN DMN score decline through the AD progression (Spreng and Turner, 2013). The mechanism may be the activity-dependent or metabolism-dependent pathology hypothesis: the DMN's continuous activity may lead to the early formation and diffusion of the AD neuropathological hallmarks (Palmqvist et al., 2017; Buckner et al., 2005; Buckner et al., 2009). To be specific, we found an increased structural association between the EC and MTG in Group 2 and decreased structural association between EC and MTG as well as SFG in Group 3. Although no significant difference in Group 1, these subjects show the trend of an increased structural association involving the temporal and frontal regions. These changes could be described as a biphasic trajectory which was resulted by neuropathological progression. Moreover, such DMN changes always correlate with cognitive status and CSF level (Spreng and Turner, 2013; Allen et al., 2007; Zhang et al., 2010). One SCN study found a decreased association between EC and prefrontal region in early AD patients and proposed it as the underlying reason for cognitive deficits (Montembeault et al., 2016). Similarly, we also found that entorhinal-anchored peak clusters linked to the clinical scores in the subjects along the AD continuum. These findings highlighted the primary role of the entorhinal-anchored network (DMN medial temporal subsystem) in cognition maintenance. Conclusively, we proposed that DMN showed a structural hyperconnectivity at the early stage and then hypoconnectivity as AD progresses; furthermore, structural connectivity changes may indicate the cognition decline.

SN is in charge of diverse homeostatically relevant internal and external stimuli, and always shows alternated function in AD patients. Here, we observed a dynamic structural association in this intrinsic network: increased structural association between FIC and precuneus in Group 1 subjects, while decreased structural association in ITG in Group 3 subjects. These results are in line with one functional study, which reported firstly increased (between CDR 0 and CDR 0.5) and then
decreased correlation (at CDR 1) in SN in subjects along AD continuum (Brier et al., 2012). Similarly, the work of Schultz AP also reported hyperconnectivity in SN in subjects with amyloid positive and then hypoconnectivity when neocortical tau levels are high (Schultz et al., 2017). Conclusively, these findings suggested the dynamic changes in SN along AD neuropathological progression.

Regarding the ECN, we observed a continuously increased association in Group 1 and Group 3 subjects. Based on the previous study, we speculated it as a compensatory network associated with cognitive reservation in AD patients (Grady et al., 2003; Stern, 2006). Similar results can be found in another study which observed extensive SCN in ECN in AD patients with positive Aβ status (Montembeault et al., 2016). Our data extended this work by demonstrating a gradually increased structural association between DLPFC and frontal regions along the AD continuum. Here, stronger covariance strength between the seed and peak clusters indicated more intra-network connections to maintain cognition (Lin et al., 2016). Our further correlation analysis showed that DLPFC-anchored peak cluster volumes correlated to the cognitive performance, suggesting a compensatory clinical meaning of the DLPFC-anchored ECN in AD continuum. By coincidence, SFG presents a significant decreased structural association with the EC in AD patients. This may partially support the hypothesis that AD features opposing connectivity in the DMN and ECN (Zhou et al., 2010; Agosta et al., 2012).

The DMN, SN, and ECN showed interactive and dynamic changes with neuropathological progression. Regarding the increased structural association in DMN and SN at the early stage, possible explanations may be the compensatory processes in response to toxic effects of Aβ (Supakar et al., 2008; Zhou et al., 2010; Matura et al., 2014) or the amyloid-induced inflammatory response (Montal et al., 2018), especially in Group 1. Such inflammation would trigger changes in cell volume (neuronal and glia swelling) as well as number (glia recruitment and activation) at the early stages of AD pathology and lead to the GM volume changes (Fortea et al., 2016; Rodriguez-Vieitez et al., 2016). As the neuropathological progression, the synergy between amyloid and tau pathologies starts (Schultz et al., 2017; Pascoal et al., 2017), such compensation mechanism become gradually invalid, ending with the whole structural connectivity in chaos. This could be proved the progressively decreased cognition in Group 2 and Group 3, reflecting the progressive decomposition process.

Conclusively, our study suggested a dynamic SCN pattern changes along the temporal pathological accumulation. As the AD progresses, the DMN and SN showed phases of hyperconnectivity and then hypoconnectivity while ECN showed the potentially compensatory role of the ECN in AD patients.

5. Limitation

There were some limitations to this study. Firstly, our study is cross-sectional research. Although we try to use the subjects with different disease stages to depict the AD continuum, a further longitudinal study should be done. Moreover, our SCN analysis was constructed in a group level which may not allow the assessment of the relationship between single-subject gray matter network measures with cognition. Further SCN analysis based on single-subject should be done.

Ethics approval and consent to participate

All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional and national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards. Written informed consent was obtained from all participants and authorized representatives, and the study partners before any protocol-specific procedures were carried out in the ADNI study. More details in http://www.adni-info.org.

Consent for publication

Not applicable.

Availability of data and material

The datasets generated and analyzed during the current study are available in the ADNI study. More details in www.adni-info.org.

Acknowledgments

KL designed the study and wrote the first draft of the manuscript. KL analyzed the MRI data and wrote the protocol. QZ and JX collected clinical and MRI data. JZ, CW, XX, PH, ZS and MZ assisted with study design and interpretation of findings. All authors have contributed to and approved the final manuscript. All authors read and approved the final manuscript. The authors declare no conflict of interest.

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Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.nicl.2019.101828.

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