Accuracy of calculating mechanical power of ventilation by one commonly used equation

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Received: 4 October 2021 / Accepted: 29 January 2022 / Published online: 15 April 2022
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Abstract
Gattinoni’s equation, MPrs = 0.098 × RR × \[ V_T \left( \frac{1}{2} E_{rs} + \frac{RR \times \frac{1+I:E}{60\times I:E}}{R_{aw}} \right) + V_T \times PEEP \], now commonly used to calculate the mechanical power (MP) of ventilation. However, it calculates only inspiratory MP. In addition, the inclusion of PEEP in Gattinoni’s equation raises debate because PEEP does not produce net displacement or contribute to MP. Measuring the area within the pressure–volume loop accurately reflects the MP received in a whole ventilation cycle and the MP thus obtained is not influenced by PEEP. The MP of 25 invasively ventilated patients were calculated by Gattinoni’s equation and measured by integration of the areas within the pressure–volume loops of the ventilation cycles. The MP obtained from both methods were compared. The effects of PEEPs on MP were also evaluated. We found that the MP obtained from both methods were correlated by \( R^2 = 0.75 \) and 0.66 at PEEP 5 and 10 cmH2O, respectively. The biases of the two methods were 3.13 (2.03 to 4.23) J/min (\( P < 0.0001 \)) and −1.23 (−2.22 to −0.24) J/min (\( P = 0.02 \)) at PEEP 5 and 10 cmH2O, respectively. These P values suggested that both methods were significantly incongruent. When the tidal volume used was 6 ml/Kg, the MP by Gattinoni’s equation at PEEP 5 and 10 cmH2O were significantly different (4.51 vs 7.21 J/min, \( P < 0.001 \)), but the MP by PV loop area was not influenced by PEEPs (6.46 vs 6.47 J/min, \( P = 0.331 \)). Similar results were observed across all tidal volumes. We conclude that the Gattinoni’s equation is not accurate in calculating the MP of a whole ventilatory cycle and is significantly influenced by PEEP, which theoretically does not contribute to MP.

Keywords Acute respiratory distress syndrome · Mechanical power · Mechanical ventilation · Positive end-expiratory pressure · Respiratory failure · Ventilator-induced lung injury · Work of breathing

Abbreviations
ARDS Acute respiratory distress syndrome
Ers Elastance of respiratory system
I:E Inspiratory to expiratory ratio
MP Mechanical power
PEEP Positive end-expiratory pressure

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$P_{\text{peak}}$  Peak airway pressure  
$P_{\text{plat}}$  Plateau pressure  
Raw  Airway resistance  
PV  Pressure–volume  
RR  Respiratory rate  
VILI  Ventilator-induced lung injury  
$V_T$  Tidal volume

### 1 Introduction

In 2016, Gattinoni et al. proposed a hypothesis that mechanical power (MP) delivered to the mechanically ventilated patients contributes to their ventilator-induced lung injury (VILI). Since the MP is hard to measure directly in clinical practice, they invented a formula to estimate the MP by algebraic calculation. Their equation incorporates several routinely monitored ventilator parameters and is written as:

$$MP_{rs} = 0.098 \times RR \times V_T \times \left[ \frac{V_T^2}{2} \left( \frac{1}{E_{rs}} + \frac{1}{60 \times I:E} \right) + \frac{V_T \times PEEP}{2} \right],$$

where $MP_{rs}$ is the MP received by the respiratory system, 0.098 is the conversion factor from L*cmH$_2$O to Joule, RR is respiratory rate, $V_T$ is the tidal volume, $E_{rs}$ is the elastance of the respiratory system, $I:E$ is the inspiration to expiration ratio, $R_{aw}$ represents airway resistance and PEEP is the value of positive end-expiratory pressure. The equation can also be simplified to read:

$$MP_{rs} = 0.098 \times RR \times V_T \times \left[ \frac{P_{\text{peak}} - \frac{1}{2}(P_{\text{plat}} - PEEP)}{2} \right],$$

where $P_{\text{peak}}$ is the peak inspiratory airway pressure and $P_{\text{plat}}$ is the plateau pressure. Please refer to their original article for details of derivation of these equations [1].

Since its publication, this calculation equation has gained wide acceptance. It has been adopted as a reference standard for comparison with new MP estimation methods [2, 3]. It was also commonly used in clinical studies to examine the correlation between MP and outcomes of various kinds of patients [4–6].

Nevertheless, Gattinoni’s equation calculates only the work of inspiration. It was verified by comparing with the measured area between inspiratory pressure curve and volume axis, which represents the inspiratory work only (Fig. 1D). Gattinoni admitted that expiration ‘very possibly’ also contributes to MP [7, 8]. Actually, expiration is an integral part of a respiratory cycle and exerts its own

![Fig. 1](https://example.com/fig1.png)  
**Fig. 1** The work done by a physiologic pathway with hysteresis is the area enclosed by a PV loop. The work done during left ventricular systole is shown in (A), and the work during left ventricular diastole is shown in (B). Net work of a cardiac cycle is the work of systole subtracting that of diastole (C). By the same principle, the work done by inspiration (D) subtracting that of expiration (E) results in a net work of a respiratory cycle (F). Both net works of a cardiac and respiratory cycle are the hysteresis areas of PV loops.
mechanical work in a direction opposite to that of inspiration. So, the network of a tidal ventilation is obtained by subtracting the expiratory from the inspiratory works (Fig. 1E and F). Mechanical work of a complete tidal ventilation cycle, including both inspiratory and expiratory parts, is graphically represented by the hysteresis area surrounded by a pressure–volume (PV) loop [9, 10]. For any displacement with hysteresis, the work done is measured by the area enclosed in the loop of the movement path. This principle also holds true in the realms of thermodynamics [11] and cardiac physiology [12]. Theoretically, this measurement of mechanical work (or MP) is more accurate than those considering only one limb of hysteresis.

Considering only inspiratory limb also raises debate about including PEEP value in the calculation of work [13]. The work is defined by either force × distance, or pressure × volume. Since PEEP does not by itself produce displacement or volume change during tidal ventilation, its contribution to work is theoretically zero. If both inspiration and expiration are considered and work of ventilation is measured by the hysteresis area surrounded by PV loop, PEEP plays no role at all.

In this study, we compared MPs calculated from Gattinoni’s equation with those obtained from measuring the hysteresis area surrounded by the PV loop to evaluate the accuracy of this equation.

2 Methods

2.1 Study design

Invasively ventilated patients admitted to the intensive care units of Changhua Christian Hospital (Changhua, Taiwan) from Aug. 2019 to Apr. 2021 were prospectively enrolled. We excluded patients under 20 or over 90 years of age, with over 60% of the inspired fraction of O₂, with Acute Physiology and Chronic Health Evaluation score over 30, with a plateau pressure over 30 cmH₂O, or with unstable hemodynamics. The study was approved by the institutional review board of Changhua Christian Hospital (Approval No. 181262). Informed consents were obtained from surrogates of all participants.

2.2 Raw data acquisition

All patients were measured by an Evita 4 ventilator (Dräger Medical, Lübeck, Germany), which was connected to a laptop with Ventview (Dräger Medical, Lübeck, Germany) software for data collection. Appropriate sedation and muscle relaxation were given to patients with spontaneous respiration. Upon measurement, ventilators were set at volume-controlled mode with a constant flow which was adjusted to avoid harmfully high airway pressure. Inspiratory time was lengthened to generate an inspiratory hold long enough for measuring plateau pressure. Various combinations of Vₜ (6, 8, and 10 ml per kg of body weight) and PEEPs (5 and 10 cmH₂O) were set during measurement. Raw data of airway pressure, flow and volume during the measurement were downloaded to the laptop via Medibus protocol with a sampling rate of 67 Hz for subsequent offline analysis.

2.3 Derivation and calculation of ventilation-related parameters

The Pplat was defined by the last pressure value at the inspiratory plateau phase with zero airflow. The PEEP value was defined by the average of all pressure data of expiratory phase starting from flow drops to −1 L/min. The Eₜ, Rₚₐₜ, RR, Vₜ, I: E and the area inside the PV loop were calculated from the downloaded raw data breath by breath using an executable program written with MATLAB 7.2 (The MathWorks, Natick, MA, USA). The work of ventilation was assessed by both Gattinoni’s equation [1] and PV loop area. The work expressed in L cmH₂O was converted to Joules by a factor of 0.098. The MP was obtained by multiplying the work per breath by the RR.

2.4 Statistical analysis

Data were expressed as number (percentage) for categorical data or median and interquartile range for continuous data. A simple regression model was performed to evaluate the correlation between MP values by Gattinoni’s equation and PV loop area. Bland–Altman analysis was used to evaluate the agreement between the two MP evaluation methods. Wilcoxon signed-rank test was used to compare two repeatedly measured works at PEEP levels of 5 and 10 cmH₂O. The SAS 9.4 software (SAS Institute Inc., Cary, NC, USA) was used for statistical analysis. A two-tailed p value less than 0.05 was considered statistically significant.

3 Results

3.1 MP by Gattinoni’s equation and PV loop area

A total of 25 patients were enrolled and their baseline clinical characteristics were listed in Table 1. When the PEEP was 5 cmH₂O, the MPs by both methods were correlated by a regression formula: MP by Gattinoni’s equation = 3.37 + 0.45 × MP by PV loop area, R² = 0.75, P < 0.001 (Fig. 2A). When the PEEP was 10 cmH₂O, the regression formula was: MP by Gattinoni’s equation = 5.51 + 0.63 × MP by PV loop area, R² = 0.66, P < 0.001 (Fig. 2B). The Bland–Altman plot corresponding to PEEP 5 cmH₂O was
The mean of difference was 3.13 J/min, and the 95% confidence interval was 2.03 to 4.23 J/min (lower limit = −6.05 J/min, upper limit = 12.30 J/min). The P value for the null hypothesis (H0: mean of difference = 0) was less than 0.0001, which means that the results of both methods were significantly different. The Bland–Altman plot of PEEP 10 cmH2O was presented in Fig. 2D. The mean of difference was −1.23 J/min, and the 95% confidence interval was −2.22 to −0.24 J/min (lower limit = −9.47 J/min, upper limit = 7.01 J/min). The P value for the null hypothesis was 0.02, suggesting that the results of both methods were significantly different. The largest differences tended to be found when the mean MP was greater than 15 J/min. One of our patient’s PV loop at VT 10 ml/Kg and PEEP 10 cmH2O was plotted against the calculated area byGattinoni’s equation (Fig. 3). A prominent incongruence of both areas can be easily observed. When the whole study population was divided into those with and without acute respiratory distress syndrome (ARDS), the results were similar except for ARDS patients under PEEP 10 cmH2O where no difference could be found probably because the case number of ARDS was too small (only 7). These data could be found in our supplemental Figs. s1 and s2.

### 3.2 Assessing effects of PEEP on MP by both methods

Because PEEP does not by itself produce any air displacement during tidal ventilation, its contribution to MP is theoretically zero. The MPs, by integration of the areas inside the PV loop, were not significantly different at PEEP 5 and PEEP 10 cmH2O. On the other hand, the MPs calculated by Gattinoni’s equation, at PEEP 5 of PEEP 10 cmH2O was presented in Fig. 2D. The mean of difference was −1.23 J/min, and the 95% confidence interval was −2.22 to −0.24 J/min (lower limit = −9.47 J/min, upper limit = 7.01 J/min). The P value for the null hypothesis was 0.02, suggesting that the results of both methods were significantly different. The largest differences tended to be found when the mean MP was greater than 15 J/min. One of our patient’s PV loop at VT 10 ml/Kg and PEEP 10 cmH2O was plotted against the calculated area byGattinoni’s equation (Fig. 3). A prominent incongruence of both areas can be easily observed. When the whole study population was divided into those with and without acute respiratory distress syndrome (ARDS), the results were similar except for ARDS patients under PEEP 10 cmH2O where no difference could be found probably because the case number of ARDS was too small (only 7). These data could be found in our supplemental Figs. s1 and s2.

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**Table 1** Baseline characteristics of enrolled patients (n = 25)

| Variables                  | Number (%) or Median (IQR) |
|----------------------------|----------------------------|
| Age (year)                 | 63 (52–75)                 |
| Male (n, %)                | 17 (68%)                   |
| Height (cm)                | 160 (156–169)              |
| Body Mass Index (Kg/m²)    | 24.68 (22.73–27.78)        |
| ARDS (Y/N)                 | 7/18                       |
| Respiratory rate (min⁻¹)   | 18 (14–20)                 |
| Ventilator mode PCV: VCV   | 22:3                       |
| Monitored VT (ml)          | 542 (500–603)              |
| Driving pressure (cmH2O)   | 20 (18–22)                 |
| PEEP (cmH2O)               | 6 (5–8)                    |
| Static compliance (ml/cmH2O)| 27.1 (23.81–31.25)         |
| P arterial O2/FIO2 (mmHg)  | 271 (136–361)              |
| A-a DO2 (mmHg)             | 185 (96–315)               |
| PaCO2 (mmHg)               | 32 (25–39)                 |

A-a DO2 alveolar-arterial oxygen difference, PCV pressure-controlled ventilation, VCV volume-controlled ventilation.
cmH2O were significantly smaller than those at PEEP 10 cmH2O (Table 2). The MPs byGattinoni’s equation of ARDS patients did not differ significantly at PEEP 5 and 10 cmH2O. This may be due to small case numbers in this group.

4 Discussion

In this study, we provided evidence to challenge the accuracy and validity of Gattinoni’s equation. In his original publication, the MPs by Gattinoni’s equation were in very good correlation with the measured ones by $R^2$ of 0.96 to 0.99 and the mean biases between the two methods were minimal (around $\pm 0.5$ J/min) [1]. In contrast, our data revealed a less than perfect agreement between MPs by Gattinoni’s equation and measured ones. This discrepancy lies in the difference in MP measurement. Gattinoni’s measured areas between inspiratory pressure curve and ordinate of volume, but we measured areas surrounded by the PV loop. Gattinoni’s measurement was restricted to the inspiratory phase, while ours took both inspiration and expiration into account and was a more reliable value of the MP received during the tidal ventilatory cycle.

There is growing awareness of the important role played by expiration during a ventilatory cycle. The MP accumulated at end-inspiration is eliminated by exhaling into the atmosphere or dissipating into lung tissue during the expiratory phase [7]. Therefore, expiration surely contributes to MP and the consequential VILI. By manipulating the expiratory flow of mechanical ventilation, we can achieve more lung recruitment [14], more homogeneous lung aeration [15], better gas exchange [16], and less VILI [17]. So, neglecting expiration makes Gattinoni’s equation prone to inaccuracy in assessing the MP that a ventilated patient received.

We think the most crucial origin of inaccuracy stems from including PEEP in the calculating equation of Gattinoni’s et al. Our data demonstrated that the PEEP value did

| Table 2 Assessing effects of PEEP on mechanical power by Gattinoni’s equation and area of PV loop |
|---------------------------------------------------------------|-------------------|-------------------|-------------------|-------------------|
| Non-ARDS (n=18)                                              | Power by Gattinoni Equation (J/min) | Power by hysteresis area of PV loop (J/min) |
|                                                              | PEEP 5 cmH2O       | PEEP 10 cmH2O     | P                 | PEEP 5 cmH2O       | PEEP 10 cmH2O     | P                 |
| Vt 6 ml/kg                                                    | 5.07 (4.34, 7.56)  | 8.50 (6.94, 10.38)| <0.001            | 6.51 (4.22, 9.69)  | 6.29 (4.25, 10.27)| 0.381             |
| Vt 8 ml/kg                                                    | 7.15 (6.04, 9.82)  | 10.62 (9.63, 15.06)| 0.001             | 9.56 (6.13, 13.16)| 8.82 (7.24, 13.82)| 0.868             |
| Vt 10 ml/kg                                                   | 10.08 (7.69, 13.77)| 14.81 (12.9, 19.98)| <0.001            | 13.29 (7.94, 20.28)| 12.30 (8.56, 19.38)| 0.435             |
| ARDS (n=7)                                                    |                   |                   |                   |                   |                   |                   |
| Vt 6 ml/kg                                                    | 2.63 (1.27, 3.44)  | 2.80 (0.6, 4.72)  | 0.735             | 6.41 (2.94, 12.38)| 8.50 (4.59, 12.69)| 0.612             |
| Vt 8 ml/kg                                                    | 4.48 (3.26, 6.76)  | 4.44 (2.79, 6.44) | 0.612             | 13.99 (6.44, 17.21)| 11.83 (8.32, 14.34)| 0.091             |
| Vt 10 ml/kg                                                   | 6.59 (4.58, 11.63)| 7.80 (5.94, 8.93) | 1                 | 12.67 (10.68, 22.48)| 14.80 (6.58, 21.97)| 0.735             |
| All (n=25)                                                    |                   |                   |                   |                   |                   |                   |
| Vt 6 ml/kg                                                    | 4.51 (3.46, 7.16)  | 7.21 (3.85, 9.49) | <0.001            | 6.46 (4.21, 10.48)| 6.47 (4.33, 10.84)| 0.331             |
| Vt 8 ml/kg                                                    | 6.84 (4.62, 9.12)  | 9.97 (6.09, 13.68)| 0.001             | 9.71 (6.35, 15.38)| 9.71 (8.05, 14.15)| 0.361             |
| Vt 10 ml/kg                                                   | 9.76 (6.82, 12.25)| 13.68 (8.28, 16.49)| 0.001            | 12.98 (8.86, 21.28)| 14.52 (8.34, 19.65)| 0.607             |

Wilcoxon Signed Rank Test is a non-parametric statistical hypothesis test that compares two repeated measurements of mechanical power values. It is used to assess whether the average mechanical power rank is different between PEEP 5 and PEEP 10 cmH2O.
not influence MP measured by PV loop method, but it falsely increased the MP calculated by using Gattinoni’s equation (Table 2). As we mentioned in the introduction, incorporating a static pressure without net displacement, like PEEP, into the calculation of MP is contradictory to the basic law of physics. Moreover, Gattinoni’s equation suggested that a high PEEP can increase both the MP and the chance of subsequent VILI. However, this assumption could find support from neither animal studies nor clinical trials. High PEEPs failed to produce evidence of VILI in the lungs of the experimental animals [18, 19]. According to a metaanalysis of 8 randomized trials on ARDS patients, high PEEPs did not lead to worse clinical outcomes and can even reduce some patients’ mortality [20].

Gattinoni’s original hypothesis that MP induces VILI and subsequent poor clinical outcomes has never been unequivocally proved [8]. Studies on the clinical implications of MP were currently all observational. Some studies showed a good correlation between MP and mortality [21, 22], whereas some did not [23, 24]. Still, some studies barely established a correlation by modifying the definition of MP calculated [4, 25].

Proposing a revised version of Gattinoni’s equation is beyond the scope of this article. It cannot be done by simply subtracting PEEP from the equation. We have tried to calculate the MP of our patients by using Gattinoni’s equation without PEEP term, but the results are still unsatisfactory (Please refer to our supplement Fig. s3).

There are two limitations to our study that worth mentioning. First, our ARDS patient number was too small to draw a solid conclusion regarding this subgroup. The insignificant results from analysis within this group are all subject to type II error. Second, to avoid harmful VILI, we did not apply a $V_T$ of more than 10 ml/Kg or a PEEP over 10 cmH2O during MP measurement. Extrapolating our results beyond these $V_T$ or PEEP limitations is subject to imprecision.

In conclusion, Gattinoni’s equation is not accurate in the calculation of the MP during a whole ventilatory cycle and is significantly influenced by PEEP, which theoretically does not contribute to MP.

Supplementary Information The online version contains supplementary material available at https://doi.org/10.1007/s10877-022-00823-3.

Acknowledgements This study was supported by Grant 108-CCH-IRP-081 of Changhua Christian Hospital (Changhua, Taiwan) and Grant V96C1-153 of Taipei Veterans General Hospital (Taipei, Taiwan). We thank Mr. Jian-Nan Pan, manager of Dräger Medical (Lübeck, Germany), for technical support in MP measurement. We thank respiratory therapists Ji-Yuan Ke, Ya-Yun Chuang, and Shu-Hua Hsieh for ventilatory raw data acquisition. We thank Ms. Tzu-Ling Tsai for her secretarial assistance.

Author contributions SHW drafted the manuscript. CTK analyzed the data and performed statistical calculations. ICM, CCC, and KHL collected clinical data and took care of the study patients. CDK was involved in the conception of the study and gave final approval of the version to be published.

Funding This study was funded by Changhua Christian Hospital, (Grant No. 108-CCH-IRP-081) to Shin-Hwar Wu; Taipei Veterans General Hospital (Grant V96C1-153) to Cheng-Deng Kuo.

Declarations

Conflict of interest The authors declared that they have no competing interest.

Ethical approval The study was approved by the Institutional Review Board of Changhua Christian Hospital (Approval No. 181262).

Informed consent Informed consents were obtained from surrogates of all participants.

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