The influence of positive end-expiratory pressure (PEEP) in predicting fluid responsiveness in patients undergoing one-lung ventilation

In-Jung Jun¹, Mi Hwa Chung¹, Jung Eun Kim¹, Hye Sun Lee², Jung Mo Son¹, Eun Mi Choi¹

¹. Department of Anesthesiology and Pain Medicine, Kangnam Sacred Heart Hospital, University of Hallym College of Medicine, Seoul, Korea.
². Biostatistics Collaboration Unit, Yonsei University College of Medicine, Seoul, Korea.

Corresponding author: Eun Mi Choi, Department of Anesthesiology and Pain Medicine, Kangnam Sacred Heart Hospital, Hallym University College of Medicine, 948-1, Daerim 1-dong, Yeongdeungpo-gu, Seoul, Korea. Tel: 82-10-9057-6639, Fax: 82-2-845-1571, E-mail: emchoi96@hallym.or.kr.

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Abstract

Background: Dynamic preload parameters such as pulse pressure variation (PPV) and stroke volume variation (SVV) have widely been used as accurate predictors for fluid responsiveness in patients under mechanical ventilation. To circumvent the limitation of decreased cyclic change of intrathoracic pressure, we performed an intermittent PEEP challenge test to evaluate whether PPV or SVV can predict fluid responsiveness during one-lung ventilation (OLV).

Methods: Forty patients undergoing OLV were analyzed. Baseline hemodynamic variables including PPV and SVV and respiratory variables were recorded after chest opening in lateral position under OLV (T1). Five minutes after application of PEEP 10 cmH₂O, the parameters were recorded (T2). Thereafter, PEEP was withdrawn to 0 cmH₂O for 5 minutes (T3), and fluid loading was performed with balanced crystalloid solution 6 mL/kg of ideal body weight for 5 minutes. Five minutes after completion of fluid loading, all variables were recorded (T4). The patient was classified as fluid responder if SV increased ≥10% after fluid loading and as non-responder if SV increased <10%.

Results: Prediction of fluid responsiveness was evaluated with area under the receiver operating characteristic (ROC) curve (AUC). Change in stroke volume variation (ΔSVV) showed AUC of 0.9 (P < 0.001), 95% CI = 0.82-0.99, sensitivity = 88%, specificity = 82% for discrimination of fluid responsiveness. Change in pulse pressure variation (ΔPPV) showed AUC of 0.88 (P < 0.001), 95% CI = 0.78-0.97, sensitivity = 83%, specificity = 72% in predictability of fluid responsiveness. Cardiac index and stroke volume were well maintained after PEEP challenge in non-responders while they increased in responders.

Conclusions: ΔPPV and ΔSVV induced by PEEP challenge are reliable parameters to predict fluid responsiveness as well as very good predictors of fluid unresponsiveness during OLV.

Key words: positive end-expiratory pressure; one-lung ventilation; pulse pressure variation; stroke volume variation; fluid responsiveness; Esophageal Doppler

Introduction

Optimal fluid management during lung surgery is of significant importance and remains challenging for anesthesiologists. Generally, restrictive fluid management is recommended for lung surgery to prevent acute lung injury or impairment of respiratory gas exchange from fluid overload [1, 2]. However, maintaining adequate organ perfusion is also important for favorable outcomes. Dynamic preload parameters such as pulse pressure variation (PPV), or stroke volume variation (SVV) have been widely used as accurate predictors for fluid responsiveness in patients under mechanical ventilation [3].

During lung surgery, fluid management using dynamic parameters is complex because of physiologic alteration by opened non-dependent thorax, one-lung ventilation (OLV) and protective ventilation technique with low tidal volume. These conditions affect the ability of PPV and SVV to predict fluid responsiveness [4]. Previous studies for
evaluating the usefulness of dynamic parameters in lung surgery showed diverse results [3, 5]. In thoracic surgery with OLV, threshold value of dynamic parameters is usually lower than that of two lung mechanical ventilation because of decreased cyclic changes of intrathoracic pressure [6]. For that reason, dynamic parameters might misread for predicting fluid responsiveness under OLV. Therefore, the intermittent tidal volume challenge or PEEP challenge can be applied to evaluate whether PPV or SVV could be a guide for fluid responsiveness by increasing cyclic changes of intrathoracic pressure. However, applying high tidal volume during OLV is associated with postoperative respiratory failure and high mortality rate [7]. We chose PEEP challenge as an intermittent trial, since PEEP application could be the best way to improve intrathoracic pressure during OLV. PEEP application during OLV improves compliance and functional residual capacity of the dependent lung and improves oxygenation [8, 9].

To our knowledge, challenge test to improve the diagnostic ability of dynamic parameters have not been studied during OLV. We hypothesized that temporary increase in PEEP from 0 to 10 cmH₂O may improve predictability of dynamic parameters on fluid responsiveness during OLV.

Materials and Methods

Participants

After approval from the Institutional Review Board of Hallym University Kangnam Sacred Heart Hospital (approval number: 2018-11-028) and registration at ClinicalTrials.gov (NCT 03794414), we conducted the prospective observational study in 40 patients undergoing lung surgery under OLV (Fig. 1). The study was performed between January, 2019 and June, 2020 in our institution, and informed consent was obtained from all participants. Exclusion criteria are as follows: known preoperative cardiac disease including arrhythmia, moderate to severe valvular heart disease, moderate to severe pericardial effusion, left ventricular ejection fraction <40%, moderate to severe chronic obstructive lung disease with 1-second forced expiratory volume <60% of predicted values, contraindication to esophageal Doppler monitoring probe insertion (i.e. esophageal stent, carcinoma of the esophagus or pharynx, previous esophageal surgery, esophageal stricture, esophageal varices, pharyngeal pouch and severe coagulopathy) and severe obesity (body mass index >35 kg/m²).

Anesthesia and one-lung ventilation

On arrival to the operation room, routine hemodynamic monitoring including electrocardiography, pulse oximetry and non-invasive arterial pressure measurement were applied. Induction of anesthesia was performed with continuous infusion of propofol and remifentanil using a target-controlled infusion system to induce and maintain anesthesia. Propofol was adjusted to effect site target concentration of 2-4 mcg/mL and remifentanil was adjusted to effect site target concentration of 2-8 ng/mL. Depth of anesthesia was continuously evaluated with an entropy (GE Healthcare, Datex-Ohmeda, Helsinki, Finland), and an entropy value was maintained between 40 and 60. All patients received 0.6 mg/kg of rocuronium for muscle relaxation. When maximal suppression was reached on train-of-four stimulation, left-sided or right-sided double-lumen tube (Broncho-cath, Tyco Healthcare, Argyle, Mansfield, MA, USA) was inserted for OLV. Correct position and depth was confirmed with fiberoptic bronchoscope. Radial artery was cannulated for continuous arterial blood pressure monitoring. Forced air warmer was applied and core temperature was maintained above 36.0 °C. Following induction of anesthesia, an esophageal Doppler probe (CardioQ, Deltex Medical, Chichester, UK) was inserted into the esophagus by a well-trained anesthesiologist. The esophageal Doppler probe was placed in the optimal position by monitoring aortic visual and auditory signals displaced on the CardioQ-ODM+ monitor (Deltex Medical, Chichester, UK).

Following position change to lateral position, OLV was initiated with tidal volume of 6 mL/kg of ideal body weight, an inspired oxygen fraction of 0.5 and I:E ratio of 1:1.5 without PEEP using volume-controlled mode. Respiratory rate was adjusted to maintain end-tidal carbon dioxide partial pressure between 35 and 40 mmHg. An inspired oxygen fraction was elevated by 0.1 if oxygen saturation fell below 92%.

Hemodynamic and respiratory assessment

Heart rate, mean arterial blood pressure and PPV were recorded through the patient monitor (CARESCAPE Monitor B850; GE Healthcare). Dynamic compliance, mean airway pressure and peak inspiratory pressure were obtained from the anesthesia ventilator machine (Datex Ohmeda Avance CS Anesthesia Machine; GE Healthcare, Helsinki, Finland). Cardiac index, stroke volume and SVV were acquired from CardioQ-ODM+ monitor. PPV and SVV were calculated as follows:

\[
PPV = \frac{(PPmax - PPmin)}{(PPmax+PPmin)/2} \times 100 \%
\]

\[
SVV = \frac{(SVmax - SVmin)}{(SVmax+SVmin)/2} \times 100 \%
\]
The parameters were displayed on the CardioQ-ODM+ monitor every 10 seconds. The parameters were recorded on three consecutive respiratory cycles and averaged for statistical analysis. Each measurement was performed under stable hemodynamic state with no inotropes or vasopressors. The changes in PPV and SVV after PEEP challenge were calculated as follows:

\[
\Delta PPV = PPV_2 (PPV \text{ measured at } T2) - PPV_1 \text{ (PPV measured at } T1),
\]

\[
\Delta SVV = SVV_2 (SVV \text{ measured at } T2) - SVV_1 \text{ (SVV measured at } T1).
\]

**Study design**

The hemodynamic and respiratory parameters were recorded at 4 predetermined time points (Fig. 2). Baseline hemodynamic and respiratory parameters were recorded 20 minutes after initiation of the operation with OLV in lateral position (T1). After T1 measurement, 10 cmH\textsubscript{2}O of PEEP was applied. Five minutes after application of PEEP 10 cmH\textsubscript{2}O, the parameters were recorded (T2). Thereafter, PEEP was withdrawn to 0 cmH\textsubscript{2}O for 5 minutes and the parameters were recorded (T3). Fluid loading was performed with balanced crystalloid solution (Plasma solution A, CJ HealthCare, Seoul, South Korea) 6 mL/kg of ideal body weight for 5 minutes. Five minutes after completion of fluid loading, all parameters were recorded (T4). All measurements were made in a hemodynamically stable state with minimum or no surgical manipulation.

To determine fluid responders, stroke volume displayed on the CardioQ-ODM+ monitor was analyzed. The patient was classified as fluid responder if stroke volume increased ≥10% after fluid loading and as non-responder if stroke volume increased <10% [10].

**Statistical analysis**

Statistical analysis was performed using Medcalc\textsuperscript{®} Version 10.0.1.0. and SPSS 22 for Windows (SPSS Inc., Chicago, IL). All data are expressed as mean ± SD, median (interquartile range) or number (percentage). Comparisons of demographic data between responders and non-responders were assessed with Student’s t-test for continuous variables and Chi-square test for categorical variables. For nonparametric data analysis, Mann-Whitney U test or Fisher’s exact test were used. Comparisons of hemodynamic variables before and after PEEP challenge or fluid loading were assessed with paired t-test. For nonparametric data analysis, Wilcoxon signed rank test was used.

ROC curves were generated for PPV1, PPV2, ΔPPV, SVV1, SVV2 and ΔSVV. To determine the diagnostic ability of the variables to predict fluid responsiveness, the area under the curve (AUC = 0.5: no apparent distributional difference between the two groups, no prediction possible; 0.6≤AUC<0.7: poor discrimination; 0.7≤AUC<0.8: acceptable discrimination; 0.8≤AUC<0.9: excellent discrimination; 0.9≤AUC<1.0: outstanding discrimination; AUC=1.0: best possible prediction) were calculated and compared using Hanley-McNeil test [11, 12]. The optimal cut-off value was determined by considering the values that maximized sensitivity and specificity. In all analysis, P<0.05 was considered to be statistically significant.

A gray zone was used to determine the values which provide inconclusive information using Youden’s index. The values in the range of gray zone mean formal conclusion cannot be obtained. Inconclusive region was defined as values with a sensitivity lower than 90% or specificity lower than 90% [13].

**Sample size estimation**

The sample size was calculated using PASS (version 12, NCSS, LLC, Kaysville, Utah, USA). The sample size was determined on the basis of ROC analysis. We considered augmented PPV by PEEP challenge to predict fluid responsiveness if the area under the ROC curve was >0.8. Assuming that the null hypothesis was 0.5 (no discrimination) with type 1 error = 0.05 and type 2 error = 0.1, a minimum of 36 patients were needed. Considering a dropout rate of 10%, 40 patients were enrolled.

**Results**

**Patient characteristics**

In our study, 44 patients were assessed for recruitment. Four patients met our exclusion criteria (moderate pericardial effusion, moderate chronic obstructive lung disease, severe obesity, contraindication of esophageal Doppler probe insertion), and 40 patients were analyzed (Fig. 1). 18 patients of 40 patients were responders to fluid loading and 22 patients were non-responders. There were no significant differences in the demographic and perioperative data between the responders and the non-responders except operation time and anesthesia time (Table 1).

**Hemodynamic and respiratory variables before and after PEEP challenge**

Hemodynamic and respiratory variables at baseline (T1) and after PEEP challenge (T2) are described in Table 2. PPV and SVV increased after PEEP challenge in responders (P<0.001). Dynamic compliance, mean airway pressure and peak
inspiratory pressure increased significantly in responders and non-responders after PEEP challenge. Cardiac index and stroke volume were well maintained after PEEP challenge compared to the baseline in non-responders while they increased in responders.

### Hemodynamic and respiratory variables before and after fluid loading

Hemodynamic and respiratory variables before (T3) and after fluid loading (T4) are described in Table 3. PPV and SVV decreased after fluid loading in responders. Hemodynamic variables including cardiac index and stroke volume increased significantly after fluid loading in responders. There were no significant difference in heart rate and mean arterial pressure in both responders and non-responders.

#### ROC analysis

Prediction of fluid responsiveness was evaluated using ROC analysis (Table 4, Figs. 3 and 4). The threshold of PPV1, PPV2, ΔPPV, SVV1, SVV2 and ΔSVV were used to determine responders and non-responders with ROC analysis. ΔSVV showed successful discrimination of fluid responsiveness (AUC = 0.9, 95% CI = 0.82-0.99, P < 0.001, cut-off value > 0%, sensitivity = 88%, specificity = 82%, (+) predictive value = 80, 95% CI = 0.006-0.99, (-) predictive value = 90, 95% CI = 76-100). ΔPPV showed AUC of 0.88 (95% CI = 0.78-0.97, P < 0.001, cut-off value > 0%, sensitivity = 88%, specificity = 72%, (+) predictive value = 71, 95% CI = 52-90, (-) predictive value = 84, 95% CI = 67-100) and SVV2 showed AUC of 0.85 (95% CI = 0.73-0.97, P < 0.001, cut-off value > 4%, sensitivity = 88%, specificity = 72%, (+) predictive value = 80, 95% CI = 0.73-0.97, (-) predictive value = 80, 95% CI = 67-100). For ΔSVV and ΔPPV were very good predictors of fluid unresponsiveness during OLV. AUC of PPV2 in predicting fluid responsiveness was 0.79 (P < 0.001). However, PPV1 and SVV1 did not predict fluid responsiveness.

### Gray zone analysis

The inconclusive region of dynamic parameters (PPV1, PPV2, ΔPPV, SVV1, SVV2, ΔSVV) to predict fluid responsiveness was depicted using gray zone analysis (Figs. 5 and 6). By determining the resampled populations, optimal threshold was obtained (Fig. 5A, B, C), (Fig. 6A, B, C). Using the alternative approach of splitting the ROC curve into the curves with sensitivity and specificity, an inconclusive zone was retrieved (Fig. 5D, E, F), (Fig. 6D, E, F). The gray zone of PPV1 was between 3.6 and 9.1 with 33 numbers of patients. However, by PEEP application, the gray zone of PPV2 decreased from 3.9 to 5.9 with 14 numbers of patients. ΔPPV showed narrowest gray zone (-0.35 to 0.75) and only 8 patients were included. The gray zone of SVV1 was between 2.3 and 7.9 with 31 numbers of patients. By PEEP application, the gray zone of SVV2 also decreased from 4.3 to 6.8 with 12 numbers of patients. ASVV showed gray zone from -0.1 to 1.3 and 16 patients were included.

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**Table 1. Demographic and perioperative data**

| Variables* | Responders (n = 18) | Non-responders (n = 22) | P-value |
|------------|---------------------|-------------------------|---------|
| Age (years) | 48 ± 20.9           | 57.8 ± 16.8             | 0.113   |
| Gender (male/female) | 16/2                  | 14/8                    | 0.082   |
| Height (cm)  | 168.6 ± 7.6          | 162.9 ± 11.2            | 0.077   |
| Weight (kg)  | 61.2 ± 8.6           | 64.9 ± 12.1             | 0.264   |
| Ideal body weight (kg) | 63.4 ± 7.5                  | 57.8 ± 12.3             | 0.098   |
| Body mass index (kg/m²) | 22.1 ± 2.4                    | 23.0 ± 3.7              | 0.362   |
| Hypertension | 4 (22)                | 6 (27)                  | 0.503   |
| Operation time (min) | 125.06 ± 71.6           | 209.8 ± 94.3            | 0.002   |
| Anesthesia time (min) | 175.9 ± 82.9             | 264.1 ± 101.4           | 0.004   |
| Intraoperative fluid amount (mL) | 1061.1 ± 426          | 1297.1 ± 535.9          | 0.129   |
| Operation type (Open thoracotomy/ video-assisted thoracic surgery) | 0/18                  | 2/20                    | 0.492   |
| Side of the operation (Right/Left) | 13/5                  | 14/8                    | 0.564   |

*Data are shown as mean ± standard deviation or number (percentage).

**Table 2. Hemodynamic and respiratory variables at baseline and after PEEP challenge**

| Variables* | Baseline (T1) | PEEP challenge (T2) | Change | P-value |
|------------|---------------|---------------------|--------|---------|
| Heart rate (beats/min) | 78.7 ± 15.8  | 81.1 ± 15.5         | 2.4 ± 5.5 | 0.085   |
| Mean arterial pressure (mmHg) | 91.9 ± 15.3  | 84.6 ± 17.0          | -7.3 ± 8.5 | 0.002   |
| Heart rate/respiratory rate ratio | 6.2 ± 1.1  | 6.3 ± 1.2           | 0.2 ± 0.4 | 0.075   |
| Dynamic compliance | 23.8 ± 6.1  | 26.9 ± 7.9          | 3.1 ± 5.4 | 0.025   |
| Mean airway pressure (cmH2O) | 7 (7-8) | 14 (13-14.3)        | 7 (6-7.3) | <0.001   |
| Peak inspiratory pressure (cmH2O) | 18.2 ± 3.5  | 23.2 ± 2.7          | 5.1 ± 1.3 | <0.001   |
| Cardiac index (L/min/m²) | 27.1 ± 0.6  | 29.0 ± 0.7          | 0.3 ± 0.4 | 0.013   |
| Stroke volume (mL) | 58.3 ± 12.9  | 63.7 ± 16.8         | 5.4 ± 7.3 | 0.006   |
| Pulse pressure variation (%) | 5.4 ± 1.8  | 7.3 ± 2.9           | 1.9 ± 1.7 | <0.001   |
| Stroke volume variation (%) | 5.5 ± 2.4  | 7.8 ± 3.3           | 2.3 ± 1.7 | <0.001   |

*Data are shown as mean ± standard deviation or median (interquartile range).

Abbreviation: PEEP: positive end-expiratory pressure.
Discussion

In our study, PEEP challenge maneuver from 0 to 10 cmH$_2$O increased the diagnostic ability of PPV and SVV of predicting fluid responsiveness during OLV. Particularly, ΔPPV and ΔSVV induced by PEEP application were accurate predictors of fluid responsiveness.

Previous studies have noted the usefulness of PPV and SVV as predictors of fluid responsiveness during mechanical ventilation [14-16]. This is based on the heart-lung interaction during positive pressure
mechanical ventilation. Positive pressure derived from mechanical ventilation induces cyclic changes in the right and left heart volume loads [17]. The wide changes in stroke volume during mechanical ventilation means the patient is likely to be fluid responsive [18].

Figure 5. Gray zone analysis of PPV1, PPV2 and ΔPPV. The gray zone analysis depicted two cut-offs between which the diagnosis of fluid responsiveness was uncertain. The optimal threshold of 1,000 resampled population is shown by histograms and the gray zone (95% CI for the optimal cut-off) is represented as a gray shaded area (A, B and C). Using the alternative approach of splitting the ROC curve, the two curves (Se; sensitivity, red, solid line), (Sp; specificity, blue, dotted line) were retrieved (D, E and F). The inconclusive zone, which is more than 10% of diagnosis tolerance, is represented as a gray shaded area.
Figure 6. Gray zone analysis of SVV1, SVV2 and ΔSVV. The gray zone analysis depicted two cut-offs between which the diagnosis of fluid responsiveness was uncertain. The optimal threshold of 1,000 resampled population is shown by histograms and the gray zone (95% CI for the optimal cut-off) is represented as a gray shaded area (A, B and C). Using the alternative approach of splitting the ROC curve, the two curves (Se; sensitivity, red, solid line), (Sp; specificity, blue, dotted line) were retrieved (D, E and F). The inconclusive zone, which is more than 10% of diagnosis tolerance, is represented as a gray shaded area.
Table 3. Hemodynamic and respiratory variables before and after fluid loading

| Variables* | Second baseline (T1) | After fluid loading (T4) | Change | \(P\)-value |
|------------|---------------------|--------------------------|--------|-------------|
| Heart rate (beats/min) | | | | |
| Responders | 79.2 ± 15.5 | 79.4 ± 14.6 | 0.2 ± 6.9 | 0.920 |
| Non-responders | 69.3 ± 8.8 | 68.3 ± 9.7 | -1.0 ± 4.1 | 0.269 |
| Mean arterial pressure (mmHg) | | | | |
| Responders | 84.4 ± 13.4 | 83.1 ± 13.5 | -1.3 ± 7.4 | 0.452 |
| Non-responders | 87.8 ± 14.0 | 88.7 ± 10.6 | -0.9 ± 6.9 | 0.566 |
| Heart rate/respiratory ratio | | | | |
| Responders | 6.2 ± 1.3 | 6.2 ± 1.1 | -0.0 ± 0.5 | 0.913 |
| Non-responders | 5.5 ± 0.8 | 5.4 ± 0.8 | -0.1 ± 0.3 | 0.263 |
| Dynamic compliance | | | | |
| Responders | 23.9 ± 7.7 | 23.0 ± 6.0 | -0.9 ± 3.9 | 0.354 |
| Non-responders | 22.3 ± 4.5 | 21.0 ± 4.2 | -1.3 ± 1.5 | <0.001 |
| Mean airway pressure (cmH\(_2\)O) | | | | |
| Responders | 7.1 ± 1.2 | 7.3 ± 1.4 | 0.2 ± 0.4 | 0.042 |
| Non-responders | 7.1 ± 1.1 | 7.2 ± 1.1 | 0 (0.0) | 0.162 |
| Peak inspiratory pressure (cmH\(_2\)O) | | | | |
| Responders | 17.4 ± 3.2 | 18.5 ± 3.5 | 1.1 ± 0.9 | <0.001 |
| Non-responders | 17.9 ± 3.4 | 18.8 ± 3.3 | 0.9 ± 0.9 | <0.001 |
| Cardiac index (L/min/m\(^2\)) | | | | |
| Responders | 2.9 ± 0.7 | 3.4 ± 0.9 | 0.5 ± 0.7 | 0.006 |
| Non-responders | 2.9 ± 0.9 | 3.1 ± 0.8 | 0.1 ± 0.3 | 0.138 |
| Stroke volume (mL) | | | | |
| Responders | 63.1 ± 17.2 | 77.2 ± 16.8 | 14.1 ± 8.5 | <0.001 |
| Non-responders | 72.3 ± 17.7 | 74.3 ± 17.5 | 1.9 ± 6.4 | 0.166 |
| Pulse pressure variation (%) | | | | |
| Responders | 5.8 ± 2.4 | 4.2 ± 2.1 | -1.6 ± 1.2 | <0.001 |
| Non-responders | 5.6 ± 1.8 | 5.1 ± 1.4 | -0.6 ± 1.4 | 0.056 |
| Stroke volume variation (%) | | | | |
| Responders | 5.7 ± 2.4 | 4.2 ± 1.9 | -1.6 ± 1.2 | <0.001 |
| Non-responders | 5.2 ± 2.5 | 4.7 ± 2.3 | -0.5 ± 1.7 | 0.143 |

*Data are shown as mean ± standard deviation.

In thoracic surgery, a difference in dynamic indices between responders and non-responders may be small or erratic by several reasons. During lung surgeries under OLV, the non-ventilated lung does not generate cyclic changes in intrathoracic pressure and the operating side of the chest is opened. Hence, wide range of the pressure generated from mechanical ventilation is transmitted to the atmosphere [19]. Additionally, the patient develops 20% to 30% of intrapulmonary shunt in the non-dependent lung after hypoxic pulmonary vasoconstriction [20]. Shunt does not take part in cyclic changes of stroke volume and the amount of pulmonary shunt left in the non-dependent lung would decrease the value of dynamic indices. For another reason, protective ventilation with small tidal volume under OLV produces reduced variations in pleural and trans-pulmonary pressure which decrease the cyclic changes in dynamic indices [6, 19]. For these reasons, PPV threshold to predict fluid responsiveness is reported to be lower during OLV [3].

To overcome the several limited conditions which make dynamic parameters unreliable as predictors of fluid responsiveness, tidal volume challenge is widely used. Transient increase of tidal volume from 6 to 8 mL/kg for 1 minute increases PPV value by more than 3.5% which reliably increases the predictive ability of PPV on fluid responsiveness [21]. Since applying high tidal volume may be harmful during OLV, we performed PEEP challenge by increasing intrathoracic pressure of the dependent lung. PEEP application increases pleural pressure and trans-pulmonary pressure which decreases right ventricular (RV) preload and increases RV afterload. During OLV, pleural pressure of closed dependent pleura may still take part in cyclic changes of intrathoracic pressure and affect RV preload. Consequently, higher level of PEEP results in greater cyclic changes in stroke volume which causes higher PPV and SVV [22]. In the present study, although baseline PPV and SVV were low, the values increased after PEEP application in fluid responders. Similarly, Lee et al. reported that PPV in group of protective OLV with PEEP of 5 cmH\(_2\)O can predict fluid responsiveness while PPV failed to predict fluid responsiveness during conventional OLV without PEEP [3]. Fu et al. also reported that PPV and SVV can predict fluid responsiveness during protective OLV with PEEP of 5 cmH\(_2\)O compared to conventional OLV without PEEP [19]. The authors showed the role of PEEP to increase the intrathoracic pressure as an explanation. Though, there is a difference that they used PEEP as an initial ventilator setting and we applied PEEP as an intermittent trial.

Table 4. Prediction of fluid responsiveness by the ROC curves of variables measured before or after fluid loading

| | AUC (95% CI) | \(P\)-value | Cut-off value, % | Sensitivity (95% CI) | Specificity (95% CI) | (+) predictive value (95% CI) | (-) predictive value (95% CI) |
|---|---|---|---|---|---|---|---|
| PPV \(_1\) | 0.51 (0.33-0.69) | 0.902 | 6 | 83 (66-100) | 31 (22-51) | 50 (32-67) | 70 (41-98) |
| PPV \(_2\) | 0.79 (0.66-0.93) | <0.001 | 5 | 83 (66-100) | 68 (48-87) | 68 (48-87) | 83 (66-100) |
| ΔPPV | 0.88 (0.78-0.97) | <0.001 | 0 | 83 (66-100) | 72 (54-91) | 71 (52-90) | 84 (67-100) |
| SVV \(_1\) | 0.57 (0.39-0.75) | 0.459 | 6 | 38 (16-61) | 86 (72-100) | 70 (41-98) | 63 (46-80) |
| SVV \(_2\) | 0.85 (0.73-0.97) | <0.001 | 4 | 94 (83-100) | 63 (43-83) | 68 (49-86) | 93 (80-100) |
| ΔSVV | 0.9 (0.82-0.99) | <0.001 | 0 | 88 (74-100) | 82 (65-97) | 80 (62-97) | 90 (76-100) |

Abbreviation: ROC: receiver operating characteristic, AUC: area under the curve, CI: confidence interval, PPV: pulse pressure variation at baseline (T1), PPV: pulse pressure variation during PEEP (positive end-expiratory pressure) challenge, ΔPPV: change in pulse pressure variation after PEEP challenge, SVV: stroke volume variation at baseline (T1), ΔSVV: change in stroke volume variation after PEEP challenge.
The present study has the clinical implication that the simple PEEP application for short period of time improved the predictive power of PPV and SVV of fluid responsiveness in patients within the gray zone. Also, there was no decrease in cardiac index and stroke volume with optimal level of PEEP application. Rather, cardiac index and stroke volume increased only in fluid responders after PEEP application. It is not clear but we assume it is associated with hypoxic pulmonary vasoconstriction since PEEP (5 to 10 cmH2O) application to the dependent lung is known to help reduce blood flow to the nondependent lung. High level of PEEP (15-20 cmH2O) is known to decrease cardiac output, although the precise mechanism to PEEP during OLV is not simple and the intrathoracic response appear multiple and complex [23].

There are several limitations with the present study. First, the total number of patients may not be sufficient to generalize our result to all patients. Further studies with larger number of patients calculated with precise parameter are needed to describe the physiologic mechanism of PEEP on dynamic parameters during OLV. Second, we used esophageal Doppler for measurement of dynamic parameters. Esophageal Doppler probe frequently needed repositioning during the operation. However, we measured cardiac output when optimal signal from descending aorta was obtained with minimum surgical manipulation. Several studies have evaluated the use of esophageal Doppler during OLV and validated its use of measuring cardiac output compared to standard method of thermodilution [24-26]. Third, operation time and anesthesia time were statistically significantly different between the responders and non-responders. Since parameters were measured at the beginning of the operation, operation time is irrelevant with the result. Fourth, two types of surgeries (video-assisted thoracic surgery, open thoracotomy) were included for two types of surgeries (video-assisted thoracic surgery and esophagectomy). Semin Cardiothorac Vasc Anesth. 2014; 18: 38-46. Fifth, although two patients underwent open thoracotomy, further study including either one type of surgery may be warranted.

In conclusion, the present study demonstrates that PEEP challenge maneuver increased the diagnostic ability of PPV and SVV of predicting fluid responsiveness and fluid unresponsiveness during OLV. The use of ΔPPV and ΔSVV after PEEP challenge would be helpful to guide fluid management in patients under OLV.

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**Competing Interests**

The authors have declared that no competing interest exists.

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