Regional homogeneity in cognition with frontal lobe injury-A resting-state fMRI study

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Abstract

Objective: To investigate the spontaneous brain activity changes with the cognitive disorders of traumatic brain injury in the frontal lobe using resting-state fMRI and regional homogeneity (ReHo).

Methods: Thirteen frontal lobe injuries with cognition impairment were sampled as traumatic brain injury group (TBIs) and fourteen healthy persons as the normal control group (NCs). General cognition was assessed through Mini-Mental State Examination (MMSE). Resting-state fMRI and T1-weighted imaging data were then collected. The ReHo maps were obtained from resting-state fMRI, and two-sample t-test was performed between the two groups. Finally, pearson correlation analysis was conducted between ReHo values extracted from different brain regions and MMSE scores of the patients.

Results: Compared with the NCs group, the TBI group showed significantly increased ReHo in the left superior frontal gyrus, right middle occipital, right declive (p < 0.05) and significantly decreased ReHo in the left media frontal gyrus, left anterior cingulate, inferior frontal gyrus, right superior temporal, right supramarginal gyrus, right hippocampus/parahippocampal, left/right supplement motor area, right uvula (p < 0.05). In addition, a positive correlation was found between the ReHo index of the left superior frontal gyrus and the MMSE scores across all patients with TBI.

Conclusions: The ReHo method may provide an objective biomarker for evaluating the functional abnormality of the cognition in frontal lobe injuries. The cognitive disorders may be related to abnormal brain activity, and the imbalance of the neural network caused by the abnormal spontaneous neuronal activity may underlie the potential cognitive damage in the frontal lobe injury.

Introduction

Traumatic brain injury (TBI) is an important public health problem, featuring high morbidity rate, disability rate and mortality rate [1], which therefore contributes to considerable social and economic costs [2]. Clinically, most TBIs result in damage to frontal lobe areas due to its anatomical features, and affect frontal lobe-dependent functions [3,4]. As we all know, the frontal lobe is responsible for several cognitive functions including attention, cognitive control, long-term memory, working memory, and especially in executive function [5-7]. What’s more, executive dysfunction is strongly related to cognitive abilities included in planning, starting, carrying out, and monitoring complex behaviours that require attention, concentration, selectiveness of stimuli, abstract thinking, cognitive flexibility, self-control, and memory [8]. And all of the frontal lobe-dependent functions enable us to transform thoughts into complex behaviours, to initiate or inhibit events [9], to reflect on other people’s mental states [10], and to plan a specific approach to each objective [11]. Therefore, the deficits in frontal lobe injuries can influence cognitive functions to the extent that social and occupational impairments may happen to patients [9]. It will result in difficulties for their emotional control, social adaptation, and even the health-related quality of life [12].

In the early 1990s, functional magnetic resonance imaging (fMRI) became popular in detecting difference in magnetic susceptibility between oxygenated and deoxygenated haemoglobin which could be used as an index of local brain activity [13]. These techniques could eventually be helpful in developing imaging biomarkers of cognitive and neurobehavioral sequelae, as well as predicting outcomes and prognosis [14]. However, the application of fMRI in clinical areas has been limited due to the complex data processing and the unsteadiness of technology. Resting-state fMRI (rs-fMRI) refers to a function magnetic resonance imaging which happens when participants are conducting none intentional thinking activity, with their eyes closed, being relaxed and still. Regional homogeneity (ReHo), as an analytic method based on Kendall’s coefficient concordance (KCC), can be used to reflect synchronicity of regional local time sequence and to observe local consistency of neuron activity in the brain. Previous studies have firmly suggested that re-fMRI with ReHo play a crucial role in the pathophysiology of mTBI [15]. In addition, it has been reported that the amplitude of low-frequency fluctuation (ALFF, another analysis method for re-fMRI) in the cingulate gyrus was significantly positively related to working memory index (WMI) in the mild patient with a

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further analysis. Then time correction was carried out to ensure that participants in the scanning environment, leaving 230 time points for points were deleted for magnetization equilibrium and adaptation of Mapping (SPM8) (http://www.fil.ion.ucl.ac.uk/spm). The first 10 time Assistant for Resting-State fMRI (DPARSF) (Yan & Zang, 2010, 33, Voxel size = 3.8 mm × 3.8 mm × 4.0 mm). The subjects were asked to close their eyes and lie down, relax, stay awake, and try not to think about anything. The scanning process lasted for 8 minutes.

Clinical assessment and image acquisition

Clinical assessment was performed within 3 days before MR imaging for both patients with TBI and NCs, including GCS, MMSE and BDI. The BDI provided estimates of depressive symptoms.

A Siemens 3.0T superconductive MR scanner (Skyra, Siemens Medical, Germany) with a 12-channel phased-array head coil was used. The subjects from both the experimental group and control group received cranial MRI in the supine position, with their heads entering first. Anatomical imaging was performed using conventional MRI SE sequence scanning (T2WI, T2-FLAIR) and gradient-echo T1-weighted scanning to obtain whole-brain MRI anatomical images. Gradient-echo T1-weighted 3D anatomical image scanning (TR/TE=1900/2.26ms, FOV=256mm×256mm, Flip angle=9°, Slice thickness=1.0mm, Gap=0, Matrix=256×256, Slice=176, Voxel size=1mm×1mm×1mm.) was used for the Talairach transformation of the images and to visualize the morphology of brain structures.

Resting-state echo-planar imaging was accomplished through a single-shot gradient-echo weighted sequence to obtain BOLD brain signals (TR/TE=2000/30ms, FOV=240 mm × 240 mm, Flip angle = 90°, Slice thickness = 4.0mm, Gap = 0.8 mm, Matrix = 64 × 64, Slice = 33, Voxel size = 3.8 mm × 3.8 mm × 4.0 mm). The subjects were asked to close their eyes and lie down, relax, stay awake, and try not to think about anything. The scanning process lasted for 8 minutes.

Data analysis

The pre-processing of data was carried out by using Data Processing Assistant for Resting-State fMRI (DPARSF) (Yan & Zang, 2010, http://rfmri.org/DPARSF), which is based on Statistical Parametric Mapping (SPM8) (http://www.fil.ion.ucl.ac.uk/spm). The first 10 time points were deleted for magnetization equilibrium and adaptation of participants in the scanning environment, leaving 230 time points for further analysis. Then time correction was carried out to ensure that scanning layers obtained at different time points were corrected to be the obtained a same time point. The correction of head motion was then carried out. Participants who had more than 2 mm of translation or greater than 2° rotation in any direction during the whole fMRI scan were excluded. Next, the functional images were spatially normalized to the Montreal Neurological Institute (MNI) space with a resampling voxel size of 3×3×3 mm3. Linear trends were removed, and a temporal band-pass filter (0.01–0.08 Hz) was applied to reduce the effects of low-frequency drifts and high-frequency respiratory and cardiac noise for further ReHo analysis.

ReHo was calculated using REST 1.8 (State Key Laboratory of Cognitive Neuroscience and Learning Beijing Normal University). Viewer of REST1.8 was used to compare the voxel, peak value, MNI Coordinates between groups.

Statistical analysis

The SPSS 20.0 software package was employed to analyse participants’ age, educational qualification and MMSE scores, the results of which were calculated as “x ± s”. Two-sample t-tests were performed to explore the differences in age and duration of education between TBIs and NCs, and a p-value of less than 0.05 (two-tailed) was considered to be statistically significant. For ReHo, we compared the voxel-wise differences between groups through two-sample t-test, and the statistical analysis was asked by a map. Voxel with a p value of less than 0.05 and a cluster size of over 78 mm3 (AlphaSim corrected) demonstrated a significant difference between two groups. REST 1.8 software package was used to extract ReHo values of the brain regions which showed differences. Pearson’s correlation analysis was conducted to compare the ReHo values of different brain regions and MMSE scores.

Results

Demographic and clinical data

Demographic and clinical data are showed in table 1. Subjects from the TBIs and NCs showed no significant difference in age and years of education. All the recruited patients showed cognitive deficiency as their MMSE scores were less than 27. Besides, healthy subjects had normal MMSE scores (> 27), and patients from the TBIs had significantly higher levels of cognition impairment than healthy subjects from the NCs (p < 0.001).

ReHo analysis

Compared with NCs, patients in the TBIs showed significantly increased ReHo in the left superior frontal gyrus and right middle occipital, right declive (Figure 1 and Table 2) and decreased ReHo in the left media frontal gyrus, left anterior cingulate, left inferior frontal gyrus, right superior temporal, right supramarginal gyrus, right hippocampus/parahippocampal, left/right supplement motor area, right uvula (Figure 2 and Table 3).

Correlation analysis

A positive correlation was found between the ReHo of the left superior frontal gyrus and MMSE scores (R2 = 0.54, p < 0.001) (Figure 3).

Discussion

Currently, there has been a lack of research on the recognition of TBI models in the investigation of frontal lobe injuries despite the prevalence of focal contusions to the frontal lobe in patient with a TBI [17,18]. In our study, we recruited cognitive disorders in frontal...
Table 1. Demographic and Clinical Features between TBIs and NCs

| Groups     | Cases | Gender | Age (yr) | Education (yr) | MMSE         |
|------------|-------|--------|----------|----------------|--------------|
| TBIs       | 13    | male   | 35.14 ± 6.20 | 8.86 ± 2.12 | 20.62 ± 3.33 |
| NCs        | 14    | female | 33.83 ± 6.65 | 9.20 ± 3.42 | 28.40 ± 1.14 |
|            |       |        | 0.37      | -0.22          | -5.03        |

|            |       |        | 0.72      | 0.83           | 0.00         |

Data are presented as mean ± standard deviation or number; a p-value less than 0.05 (two-tailed) was considered to be statistically significant; a p-value more than 0.05 (two-tailed) was considered to be no statistically significant.

Table 2. Brain Regions showing significant differences in enhanced ReHo between TBIs and NCs

| Brain region                        | L/R | MNI Coordinates | voxels | ReHo TBI | ReHo NC | T    |
|-------------------------------------|-----|-----------------|--------|----------|---------|------|
| superior frontal gyrus              | L   | -6              | 57     | 36       | 127     | 1.00 ± 0.28 | 0.43 ± 0.18 | 5.37 |
| middle occipital                    | R   | 39              | -81    | 6        | 111     | 0.94 ± 0.23 | 0.40 ± 0.29 | 3.76 |
| Declive                             | R   | 15              | -90    | -27      | 98      | 0.64 ± 0.22 | 0.09 ± 0.29 | 3.99 |

MNI, Montreal Neurological Institute; x, y, z coordinates of primary peak locations in the space of MNI; t, statistical value of peak voxel; p < 0.05, cluster size >78 mm$^3$ corrected for AlphaSim multiple comparisons.

Table 3. Brain regions showing significant differences in decreased ReHo between TBIs and NCs

| Brain region                        | L/R | MNI Coordinates | voxels | ReHo TBI | ReHo NC | T    |
|-------------------------------------|-----|-----------------|--------|----------|---------|------|
| medial frontal gyrus and anterior cingulate | L   | 9               | 48     | -9       | 123     | 0.41 ± 0.34 | 0.98 ± 0.25 | -3.54 |
| inferior frontal gyrus              | L   | -51             | 39     | -3       | 78      | 0.45 ± 0.95 | 1.21 ± 0.41 | -3.74 |
| Hippocampus and parahippocampal     | R   | 33              | -21    | -12      | 78      | -0.63 ± 0.20 | -0.32 ± 0.30 | -3.28 |
| superior temporal; supramarginal gyrus | R   | 66              | -34    | 24       | 153     | -0.18 ± 0.14 | 0.29 ± 0.16 | -4.38 |
| supplemenmotor area                 | L/R | -9              | -3     | 69       | 142     | -0.03 ± 0.26 | 0.52 ± 0.26 | -4.33 |
| uvula                               | L   | -3              | -69    | -39      | 118     | -0.58 ± 0.14 | -0.13 ± 0.27 | -3.96 |

MNI, Montreal Neurological Institute; x, y, z coordinates of primary peak locations in the space of MNI; t, statistical value of peak voxel; p < 0.05, cluster size >78 mm$^3$ corrected for AlphaSim multiple comparisons.

Figure 1. Compared with NCs, the enhanced brain region of ReHo, p < 0.05, cluster size >78 mm$^3$ corrected for AlphaSim multiple comparisons.
lobe injuries by MRI examinations and we found that TBIs showed significantly increased ReHo in the left superior frontal gyrus, right middle occipital and decreased ReHo in the left media frontal gyrus, left anterior cingulate, left inferior frontal gyrus, right superior temporal, right supramarginal gyrus, right hippocampus/parahippocampal, left/ right supplement motor area and right uvula. The findings of decreased ReHo are partly consistent with Zhan's research [15].

In this paper, an important finding was increased ReHo in the left superior frontal gyrus and a positive correlation between the ReHo values and MMSE scores. These results suggest that the ReHo in superior frontal gyrus can respond to cognitive level to some extent in frontal lobe injuries, and the function of the frontal gyrus may show compensatory enhancement at the stage of cognitive impairment [19]. Olsen had also put forward that increased brain activations typically observed in survivors of TBI might represent injury-specific compensatory adaptations in everyday life situations. What's more, we think that the cognitive compensation will increase as long as the values of ReHo improve. Another finding was that the changes of spontaneous brain activity was identified to be related to a neural network, which consisted of the prefrontal cortex, premotor area, parietal lobe, anterior cingulate cortex, and supplementary motor area [20]. Moreover, Gillis [21] affirmed this neural network may influence the cognitive mechanisms of the TBIs. They designed fMRI tasks for the TBIs, which involved working memory encoding and maintenance. Those patients showed hyperactivation in the right dorsolateral prefrontal cortex, and this might be related to memory encoding.

In the present study, decreased ReHo in the left media frontal gyrus, left anterior cingulate, left inferior frontal gyrus, right hippocampus/parahippocampal were observed. Takahashi suggest that hippocampus might affect the local hippocampal function and is thought to be important for cognitive functions such as memory, executive function and verbal fluency, as well as brain functions beyond the hippocampus such as the prefrontal cortex [22]. However, the hippocampus-frontal interaction mechanism is still unclear. A study of maladaptive response to stressful military service suggests that stress could lead to reduction in hippocampus volume and connectivity with the ventromedial prefrontal cortex together [23]. This indicates that the hippocampus and the prefrontal cortex have affected each other [24]. Using rigorous permutation testing to define human brain on structural-functional relationships, Harms found that the volume of the hippocampus was correlated with clusters in left inferior frontal gyrus and the dorsal anterior cingulate cortex [25]. However, we did not find ReHo values on those regions were correlated with the MMSE scores. Furthermore, previous fMRI studies have revealed that cortical volume reductions are bilaterally prominent in frontal, temporal, and inferior parietal regions in patient with a TBI and atrophy of the right anterior cingulate may contribute to reduced performance on cognition such as executive function tasks [26]. Becker et al also demonstrated a modulation of the influence of the anterior cingulate cortex on the dorsolateral prefrontal cortex with novel task execution and they believe that the anterior cingulate cortex activity increased the dorsolateral prefrontal cortex

![Figure 2](image1.png)

Figure 2. Compared with NCs, the decreased brain region of ReHo, \( p < 0.05 \), cluster size >78 mm³ corrected for AlphaSim multiple comparisons.

![Figure 3](image2.png)

Figure 3. A positive correlation was found between the ReHo of the left superior frontal gyrus and MMSE scores.
[27]. Taking all together, the frontal lobe injuries may reduce the frontal gyrus, anterior cingulate cortex and hippocampus functions, which, in return, influenced cognitive function.

Our study also found that cerebellum is not limited to motor control [28] but is associated with cognitive function. Compared to the NCs, right decline in the TBIs was increased and right uvula was decreased. This may be related to hippocampal-cerebellar interactions which can functionally improve cognitive collaborations [29].

In conclusion, the ReHo method may provide an objective biomarker for evaluating the functional abnormality of the cognition in frontal lobe injuries. The cognitive disorders with frontal lobe injuries demonstrated abnormal spontaneous neuronal activities. And the imbalance of the neural network caused by the abnormal neuronal activity may underlie the potential cognitive damage.

This study has several limitations. First, the sample size was relatively small. A larger sample size is needed to increase the reliability in future studies. Second, cognitive assessment was incomplete, and the memory function and executive function will be further assessed. Third, the results of ReHo only reflect function in patients with TBI. In the future we will design both the Diffusion Tensor Imaging (DTI) and rs-fMRI to explore the relationship between structural and functional deficits.

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