A novel method for vaginal cylinder treatment planning: a seamless transition to 3D brachytherapy

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Abstract

Purpose: Standard treatment plan libraries are often used to ensure a quick turn-around time for vaginal cylinder treatments. Recently there is increasing interest in transitioning from conventional 2D radiograph based brachytherapy to 3D image based brachytherapy, which has resulted in a substantial increase in treatment planning time and decrease in patient throughput. We describe a novel technique that significantly reduces the treatment planning time for CT-based vaginal cylinder brachytherapy.

Material and methods: Oncentra MasterPlan TPS allows multiple sets of data points to be classified as applicator points which has been harnessed in this method. The method relies on two hard anchor points: the first dwell position in a catheter and an applicator configuration specific dwell position as the plan origin and a soft anchor point beyond the last active dwell position to define the axis of the catheter. The spatial location of various data points on the applicator’s surface and at 5 mm depth are stored in an Excel file that can easily be transferred into a patient CT data set using window operations and then used for treatment planning. The remainder of the treatment planning process remains unaffected.

Results: The treatment plans generated on the Oncentra MasterPlan TPS using this novel method yielded results comparable to those generated on the Plato TPS using a standard treatment plan library in terms of treatment times, dwell weights and dwell times for a given optimization method and normalization points. Less than 2% difference was noticed between the treatment times generated between both systems. Using the above method, the entire planning process, including CT importing, catheter reconstruction, multiple data point definition, optimization and dose prescription, can be completed in ~5-10 minutes.

Conclusion: The proposed method allows a smooth and efficient transition to 3D CT based vaginal cylinder brachytherapy planning.

Key words: vaginal brachytherapy, high-dose-rate brachytherapy.
A novel solution to this, which allows for the transition from 2D to 3D brachytherapy, but keeps planning time down, takes advantage of the fact that radiation dose prescription as well as treatment plan reporting criteria are linked to the applicator rather than a patient specific anatomical point (viz. cylinder surface or at a depth of 5 mm into tissue). This allows for the creation of a treatment plan library in which the spatial coordinates for a set of dose points can be stored according to cylinder diameter, quickly recalled and overlaid on the patient’s actual CT data set in a timely manner for dose prescription and plan evaluation. This process has worked with great success to keep planning times to a minimum.

Over the last several years, new TPSs like Oncentra MasterPlan (ver. 3.3 SP3 from Nucletron B.V., Waardgelder 1, 3905TH Veenendaal, PO Box 930, 3900 AX Veenendaal, The Netherlands) have been introduced to facilitate the transition from 2D to 3D HDR brachytherapy. Unfortunately, the Oncentra MasterPlan TPS does not yet have an option to create a standard treatment plan library as outlined above. Each individual plan thus has to be developed from scratch, leading to substantially longer planning times.

We describe a simple, quick and efficient method for converting a pre-existing treatment plan library from Plato ver. 14.3.5 TPS (a precursor) to the Oncentra MasterPlan system (ver. 3.3 SP3) and enhancing it further, so that it can even be overlaid on the patients CT data set and further customized to each particular patient, if needed. These plans contain all the necessary dose points for dose prescription, as well as plan evaluation. We expect a significant reduction in planning time as well as potential reductions in planning error and meaningful improvements in patient throughput. Moreover, the system makes it feasible to use volumetric indices for plan evaluation using the base 3D CT data set.

**Material and methods**

Every CT scan has its own coordinate system called patient coordinate system that employs a DICOM origin, the location of which depends on the patient positioning during CT scanning. Because of its variability from patient to patient, this coordinate system is not very useful for the incorporation of standard treatment plans. Oncentra MasterPlan also supports applicator coordinate system which utilizes a user defined origin. This user-defined origin is associated with the treatment applicator and can be easily changed by the treatment planner. Since the radiation delivery in these patients is associated with the dose delivery to the applicator cylinder surface or 5 mm from it, the applicator coordinate system is more useful for the creation of standard treatment plan library. In addition, it can have multiple datasets associated to it allowing a creation of two separate sets of data points at the applicator surface and at a depth of 5 mm satisfying the ABS reporting guidelines for the endometrial cancers [9].

**Creation and importation of a plan library from Plato TPS**

The physicians at our institution are comfortable with the treatment plans that were previously created on Plato TPS (ver. 14.2) and in clinical use since more than a decade [6]. Thus, it was important to create standard treatment plans on Oncentra MasterPlan TPS with the same loading pattern and dose points defined on the applicator surface and at 5 mm. On Plato TPS, applicator points were defined on the surface of the cylinder while dose points were defined at 5 mm from the cylinder surface. Grouping of the points in this way was needed for operational purposes as Plato TPS did not support sub-classification of these points. Both points included the curve on the cylinder towards the tip of the applicator where it touches the patient’s vaginal cuff. Since this information was already available in a digital format on the Plato TPS, it was considered easier to extract and convert in a format suitable for Oncentra MasterPlan TPS. A dummy patient on Plato TPS was used to pull a standard vaginal plan from its plan library. This brought the catheter reconstruction information, dwell stepsize used, the applicator points and dose point coordinates from the standard plan into the new treatment plan. Using the “jot” program on the Plato TPS, the entire treatment plan was digitally captured in an ASCII format and saved. All of the above points (at applicator surface and at 5 mm distance from it) were correlated with the catheter reconstruction points in relation to the current origin in the plan which was recorded for proposed Oncentra MasterPlan TPS plan library. The treatment plan origin coincides with one of the active dwell position in the plan and forms the second fixed anchor point to be used during subsequent patient treatment planning on Oncentra MasterPlan TPS. The process was re-
peated for all of the stored treatment plans on the Plato TPS for various cylinder diameters and active dwell position configurations. These files were then remotely copied over to the windows environment using standard ftp commands and subsequently imported in an Excel file.

Creation of a plan library in Excel

To conform to Oncentra MasterPlan TPS coordinates system, the y and z coordinates coming from Plato TPS in the above Excel file were transposed. Additional columns were added to each point as per the Oncentra MasterPlan TPS requirement which include “Coord. System”, Act. Dose (cGy), Act. Dose (%), Normalization, Norm. Dose, Optimization, Pt. Rel. Dose and Opt. Weight. It was important to make sure that the value under the Coord. System is set to “Applicator” to ensure that these points are interpreted correctly by Oncentra MasterPlan TPS. Act. Dose (%), Norm. Dose (%), Opt. Rel. Dose, Opt. Weight columns should all have 100 as the entry as these are the default values used by Oncentra MasterPlan TPS. Actual Dose (cGy) column could contain the most common dose prescription value in use in the clinic. Normalization and optimization columns could be set to “yes” or “no” on a data set (surface or at 5 mm) depending upon the user’s preference. The actual dose prescription value and the choice of dose points for prescription and optimization (surface or at 5 mm depth from the applicator) can be changed on the fly in Oncentra MasterPlan TPS allowing for customization of the treatment plans at the time of planning. It is important that each row and column should have the data to ensure windows paste command is honored by Oncentra MasterPlan TPS.

The process was repeated for all the cylinder diameters (2.0, 2.5, 3.0 and 3.5 cm) and different number of dwell positions being used as part of proposed standard plan library. Once created and verified independently, the Excel file was password protected for any inadvertent changes. This Excel file, when used in conjunction with patients CT scan in a manner described below, can help in reproducing the standard treatment plan on to actual patient CT slices and provide the necessary points for dose prescription and evaluation to conform to MD prescription and reporting standards. This completes the base work needed to port the standard treatment plan library from Plato TPS to Oncentra MasterPlan TPS.

Recalling a plan from standard library

This new method relies on definition of three anchor points, two of which are fixed in nature while one is visual and useful to define the length of the active catheter. The first fixed anchor point is the location of first dwell position from the tip of the applicator. We still use the existing stainless steel vaginal cylinder applicators, where it is impossible to view the X-ray markers position in the CT data set and hence alternative imaging methods were needed to properly determine the first dwell position in a catheter. We acquired orthogonal radiographic films for all the cylinder diameters after setting them in a shape as if they are about to be implanted in a patient. A 5 mm bolus was wrapped around the superior end of the applicator followed by a thin copper wire, so that points at 5 mm could be seen easily on the images. We also placed standard X-ray markers in the applicator and determined the location of the first dwell point from the external tip end of the applicator. We felt it was necessary to verify this for quality assurance and documentation purposes. In our case, this distance was found to be 6.5 mm (average, range 6.25-6.75 mm). This location served as the first fixed anchor point. For clinics which have CT/MR compatible vaginal applicators, they can view the X-ray marker in the CT scan itself and can use that as the first anchor point.

When a patient comes for vaginal brachytherapy, a CT scan with the applicator in treatment position is obtained and exported to Oncentra MasterPlan TPS. These images are then imported into its database. The brachytherapy planning option within Oncentra TPS is selected and the treatment plan can now be evaluated, approved, printed and exported to the treatment unit in a standard manner. The treatment plan is also included. The table is categorized into categories and would be useful to define the length of the active catheter. The first fixed anchor point is the location of first dwell position from the tip of the applicator. We still use the existing stainless steel vaginal cylinder applicators, where it is impossible to view the X-ray markers position in the CT data set and hence alternative imaging methods were needed to properly determine the first dwell position in a catheter. We acquired orthogonal radiographic films for all the cylinder diameters after setting them in a shape as if they are about to be implanted in a patient. A 5 mm bolus was wrapped around the superior end of the applicator followed by a thin copper wire, so that points at 5 mm could be seen easily on the images. We also placed standard X-ray markers in the applicator and determined the location of the first dwell point from the external tip end of the applicator. We felt it was necessary to verify this for quality assurance and documentation purposes. In our case, this distance was found to be 6.5 mm (average, range 6.25-6.75 mm). This location served as the first fixed anchor point. For clinics which have CT/MR compatible vaginal applicators, they can view the X-ray marker in the CT scan itself and can use that as the first anchor point.

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Table 1. Standard treatment plan library with first 7 active dwell positions for 2.0 cm cylinder diameters for stainless steel vaginal cylinder applicator (Nucletron). Included are coordinates of the points on the applicator surface and at a depth of 5 mm from the applicator surface; also included is the location of the dwell position coincident with the origin of the treatment plan. It is important to know that in this table the dose values shown at cylinder surface and at 5 mm from it are for representative purposes only. Their actual values will change based on the dose-prescription, normalization as well as optimization selected by the user on the fly.

### Applicator pts – surface

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization dose (%) | Norm. dose (%) | Optimization | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|------------------------|---------------|-------------|---------------|-------------|
| A1   | 0.0    | 16.5   | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A2   | 3.5    | 15.8   | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A3   | 6.2    | 14.0   | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A4   | 8.2    | 11.5   | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A5   | 9.2    | 9.2    | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A6   | 10.0   | 5.2    | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A7   | 10.0   | 0.0    | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A8   | 10.0   | −5.0   | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A9   | 10.0   | −15.0  | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A10  | 10.0   | −10.0  | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |
| A11  | 10.0   | −20.0  | 0      | Applicator    | 1000           | 100           | no                     | 100           | no          | 100           | 100         |

### Applicator pts – 5 mm from applicator surface

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization dose (%) | Norm. dose (%) | Optimization | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|------------------------|---------------|-------------|---------------|-------------|
| A12  | 0.0    | 21.5   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A13  | 3.0    | 20.5   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A14  | 5.5    | 19.3   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A15  | 8.1    | 18.0   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A16  | 10.0   | 16.5   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A17  | 12.0   | 14.0   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A18  | 13.5   | 11.5   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A19  | 14.8   | 8.5    | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A20  | 15.0   | 5.0    | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A21  | 15.0   | 0.0    | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A22  | 15.0   | −5.0   | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A23  | 15.0   | −10.0  | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A24  | 15.0   | −15.0  | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |
| A25  | 15.0   | −20.0  | 0      | Applicator    | 700            | 100           | yes                    | 100           | yes         | 100           | 100         |

Based on the applicator diameter and number of active dwell positions used in a treatment plan. This table uses the first 7 active dwell positions from the tip of the applicator with a source step size of 5 mm. For clarity in publication, this single worksheet from the Microsoft Excel has been broken down into 4 separate tables. Similar tables were generated for different number of active dwell positions in use in the department. In this table, the most important parameters are the x, y, z coordinates of various points and their classification as “applicator points” as remaining parameters will change based on the dose-prescription, normalization and optimization selected by the user at the time of treatment planning. However, having all the items together makes it easy for the Oncentra MasterPlan to accept them using windows standard “copy” and “paste” commands. Figure 1 shows a sample treatment plan from our plan library that was generated using standard dosimetry techniques on the Oncentra MasterPlan TPS and then superimposed on a CT scan of a patient who was treated with a 3 cm vaginal cylinder. The treatment plan consists of a single catheter with first 7 active dwell positions with a step size of 5 mm. Also shown are the points defined on the applicator surface and at a depth of 5 mm. The congruence of these points in relation to applicator can be easily seen as well.
The treatment plans generated on the Oncentra Master-Plan TPS using this novel method yielded results comparable to those generated on the Plato TPS, using a standard treatment plan library in terms of treatment times, dwell weights and dwell times for a given optimization method and normalization points. A maximum of 1.4% difference was noticed between the treatment times generated among both the systems. It is important to remember that in Plato TPS the standard plan library feature has both the applicator reconstruction and definition of applicator and dose-points as a single entity. Such a rigid arrangement provides consistent results in terms of treatment times per plan once source strength has been corrected for decay. In our method on Oncentra MasterPlan TPS, definition of catheter reconstruction and applicator points are two independent events. They are combined together using user defined origin which can only be placed by using mouse. Despite maximum zooming, a slight difference between ideal and actual plan is possible due to mouse placement errors which results in slightly different results on case by case basis and explains the slight difference seen between Plato and Oncentra MasterPlan TPS results. To study the exact magnitude of these differences, 10 plans each for 2.5, 3.0 and 3.5 cm cylinder diameter were studied (we haven’t yet treated a 2.0 cm cylinder diameter patient and hence do have a CT data set of a patient).

The treatment plan library with first 7 active dwell positions for 2.5 cm cylinder diameters for stainless steel vaginal cylinder applicator (Nucletron). Included are coordinates of the points on the applicator surface and at a distance of 5 mm; also included is the location of the dwell position coincident with the origin of the treatment plan. It is important to know that in this table the dose values shown at cylinder surface and at 5 mm from it are for representative purposes only. Their actual values will change based on the dose-prescription, normalization as well as optimization selected by the user on the fly.

### Origin = 4th dwell position

**Applicator pts – surface**

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization | Norm. dose (%) | Optimi- zation | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|---------------|----------------|---------------|---------------|-------------|
| A1   | 0.0    | 21.5   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A2   | 5.0    | 20.0   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A3   | 9.3    | 16.5   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A4   | 11.8   | 11.5   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A5   | 12.5   | 5.0    | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A6   | 12.5   | 0      | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A7   | 12.5   | –5.0   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A8   | 12.5   | –10.0  | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |
| A9   | 12.5   | –15.0  | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100           | 100         |

### Applicator pts – 5 mm from applicator surface

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization | Norm. dose (%) | Optimi- zation | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|---------------|----------------|---------------|---------------|-------------|
| A10  | 0.0    | 26.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A11  | 4.5    | 25.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A12  | 9.6    | 22.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A13  | 12.5   | 20.0   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A14  | 15.5   | 16.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A15  | 16.4   | 13.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A16  | 17.0   | 10.0   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A17  | 17.5   | 5.0    | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A18  | 17.5   | 0.0    | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A19  | 17.5   | –5.0   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A20  | 17.5   | –10.0  | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
| A21  | 17.5   | –15.0  | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100           | 100         |
method as well as proposed method. The time needed to generate an acceptable treatment plan was measured using a stop watch. This time did not account for the importing CT scans as they were already in the system. Moreover, the time for pushing the treating plan to the treatment machine and printing the plan was also not included as they will be common regardless of the planning method chosen. The respective planning times were 9.3 ± 0.2 minutes vs. 4.9 ± 0.3 minutes showing an advantage of ~53%. It is important that the proposed method also improves the consistency of dose points definition at the cylinder surface, as well as at 5 mm from it and hence the dose delivery accuracy from patient to patient.

Discussion

Vaginal cylinder HDR brachytherapy has been used with increasing frequency in the treatment of endometrial cancer, cervical cancer and cancer of the vagina. Despite significant technological advances in medical imaging, external beam radiation, treatment planning and delivery, few changes have occurred in planning and delivery of vaginal cylinder brachytherapy. Though multi-channel catheter based vaginal applicators have been suggested by some users, single catheter based applicators remain the most common applicator for these treatments [12]. In the clinic, the added cost of more sophisticated CT/MR based applicators which have a limited life-expectancy and may require frequent expensive replacements, the latest 3D brachytherapy planning systems, as well as the physics/dosimetry staff required to manage them, has made it difficult to transition to 3D brachytherapy, particularly in the absence of any proven or expected clinical benefit. Despite these obstacles, there is a desire to incorporate the available 3D information in modern planning [10]. Our proposed library-based technique provides an easy method that uses existing resources to migrate from 2D to 3D brachytherapy with minimal changes in the workflow and without requiring the purchase of additional equipment. Although additional time is needed to contour organs at risk and determine dosimetric indices (for example \(D_{90}\), \(D_{150}\), \(D_{95}\)) as per GEC-ESTRO guidelines, the proposed method will significantly reduce

### Table 3. Standard treatment plan library with first 7 active dwell positions for 3.0 cm cylinder diameters for stainless steel vaginal cylinder applicator (Nucletron). Included are coordinates of the points on the applicator surface and at a distance of 5 mm; also included is the location of the dwell position coincident with the origin of the treatment plan. It is important to know that in this table the dose values shown at cylinder surface and at 5 mm from it are for representative purposes only. Their actual values will change based on the dose-prediction, normalization as well as optimization selected by the user on the fly.

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization | Norm. dose (%) | Optimization | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|---------------|----------------|---------------|--------------|-------------|
| A1   | 0.0    | 16.5   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A2   | 5.7    | 15.0   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A3   | 10.3   | 11.0   | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A4   | 12.7   | 7.7    | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A5   | 14.0   | 4.7    | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A6   | 15.0   | 0.0    | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A7   | 15.0   | –10.0  | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |
| A8   | 15.0   | –20.0  | 0      | Applicator    | 1000           | 100           | no            | 100            | no            | 100          | 100         |

| Name | x [mm] | y [mm] | z [mm] | Coord. system | Act. dose [cGy] | Act. dose (%) | Normalization | Norm. dose (%) | Optimization | Opt. rel. dose | Opt. weight |
|------|--------|--------|--------|---------------|----------------|---------------|---------------|----------------|---------------|--------------|-------------|
| A9   | 0.0    | 21.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A10  | 6.7    | 20.2   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A11  | 10.4   | 17.5   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A12  | 15.0   | 13.0   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A13  | 18.7   | 5.0    | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A14  | 20.0   | 0.0    | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A15  | 20.0   | –5.0   | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A16  | 20.0   | –10.0  | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A17  | 20.0   | –15.0  | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
| A18  | 20.0   | –20.0  | 0      | Applicator    | 700            | 100           | yes           | 100            | yes           | 100          | 100         |
The overall planning time to only slightly more than the time required for standard 2D planning. It is important to know that GEC-ESTRO indices need not be defined at the time of the treatment planning, but could be easily handled on retrospective basis as this is done for dose reporting purposes, not for modifying the treatment plans. This also may reduce treatment planning times and maintain patient throughput.

Another advantage of this method is that the process could be easily adapted for non-standard geometries that are patient and disease specific. Additional dose-points at surface or at 5 mm or at any other location could be easily added either as an extension of existing points using applicator coordinate system or even dropping them directly, using existing CT scans using patient coordinate system. This is due to the fact that the critical geometry part of defining points is on the round part towards the tip of the applicator (i.e. the first ovoid in the applicator) which is well defined by this method.

**Conclusions**

According GEC-ESTRO Guidelines, the transition from 2D to 3D image based planning for vaginal cylinder HDR brachytherapy requires segmenting of various organs at risk as well as measurement of new dose volume parameters ($D_{2cc}$, $D_{1cc}$, $D_{0.1cc}$) in addition to the standard reported 2D dose points for bladder, rectum etc. This increases planning time and effort in the absence of an expected benefit in clinical outcome. Despite this, it is important to continue supporting the transition to 3D planning, because the collection of volumetric data is an essential step in determining more accurate dose limits for organs at risk as well as for estimating the probability of treatment related toxicity. This
may allow for customization of plans to better suit patients in the future. This may even help in the comparison of multi-channel based applicators versus single catheter based applicators as well as the importance of angle of insertion (natural versus parallel to the treatment couch) of these devices in a patient’s cavity in a scientific manner.

The proposed method involves creation of a standard plan library in Microsoft Excel along with simple windows operations of “copy” and “paste”, could improve work flow efficiency, decreases overall planning time to approximately 5-10 minutes and reduces the chance for planning related errors. Though the method has been tested successfully on standard stainless steel vaginal applicator (Nucletron), it can be used with any other similar applicator as well and could be easily implemented in any Radiation Oncology department. The system is in use in our department since last 1.5 year and has been found to be very useful.

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