A hybrid functional electrical stimulation for real-time estimation of joint torque and closed-loop control of muscle activation

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Abstract

As a neuroprosthetic technique, functional electrical stimulation (FES) can restore lost motor performance of impaired patients. Through delivering electrical pulses to target muscles, the joint movement can be eventually elicited. This work presents a real-time FES system which is able to deal with two neuroprosthetic missions: one is estimating FES-induced joint torque with evoked electromyograph (eEMG), and the other is artificially controlling muscle activation with such eEMG feedback. The clinical experiment results on spinal cord injured (SCI) patients and healthy subjects show promising performance of the proposed FES system.

Keywords: Functional electrical stimulation (FES); Torque prediction; Muscle activation control; Hybrid stimulation system

Materials and Methods

System Architecture and Experiment Setup

The hybrid FES system consisted of two functional parts. The first one controls muscle activation with eEMG feedback, and the second one estimates/predicts FES-induced torque based on eEMG. Such FES system was tested on able-bodied and SCI subjects, and promising joint torque prediction and muscle activation results demonstrate its feasibility and efficiency.

Subjects

The system tests were conducted on able-bodied subjects and SCI patients upon their consent with a protocol approved by Nimes Ethics Committee, France, 2013.

System

The system consists of a wireless stimulator (emanating from a transfer of our technology to Vivaltis

for control and estimation purposes in FES. In this work, we present a hybrid real-time closed-loop FES system which both can control muscle activations and predict FES-induced torque based on eEMG. Such FES system was tested on able-bodied and SCI subjects, and promising joint torque prediction and muscle activation results demonstrate its feasibility and efficiency.
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Inc., Montpellier, France), eEMG (MP100, Biopac Systems Inc., Santa Barbara, CA, USA), torque acquisition devices (Biodex 3, Shirley Corp., NY, USA), and a laptop computer with the MATLAB (version 2012a) interface for remote control of wireless stimulator and real-time data acquisition/processing. The wireless stimulator is a regulated current dual-channel stimulator. The main features of the wireless stimulator are as follows: maximal current is 100mA with 0mA to 1mA step on a maximum load of 1kW, stimulation frequency ranges from 1Hz to 1kHz, onset pulse-width is 50ms with 1ms step, and electrical polarity can be configured according as required. Pulse width and Intensity are dynamically and remotely adjustable. The maximum pulse width for the experiment is limited to 450ms, the stimulation intensity is chosen between 25mA and 35mA, and the stimulation frequency is chosen between 30Hz–40Hz to ensure a good fusion of muscle’s contraction.

For eEMG acquisition, the bipolar AgCl EMG electrodes were positioned over the muscle belly in the direction of muscle fiber with 20mm interelectrode spacing. The reference electrode was placed on the patella of contra lateral leg. Electrical current pulses were delivered to the Tibialis (TA) or Medial Gastrocnemius (MG) muscle group with surface electrodes placed. The raw eEMG signals are acquired at a sampling frequency $f_s = 4096\text{Hz}$ through Biopac 100 system in order to capture the full range samplings of M-wave. The real-time identification and control are performed between 2 stimulation pulses so that the update and control frequency is the same as the stimulation frequency. The computation window for the eEMG is thus of the length of the period between 2 pulses i.e. around $N_{\text{win}} = f_s / f_{\text{stim}}$ where $f_s$ and $f_{\text{stim}}$ denote the eEMG sampling frequency and stimulation frequency respectively. Stimulation artifact suppression and mean-absolute operations using eEMG signals are performed.

The blanking template operation is used to suppress the stimulation artifacts, and such blanking operation is performed in every $N_{\text{win}}$ samplings of eEMG at a frequency $f_{\text{stim}}$. The mean absolute values (MAV) of the $N_{\text{win}}$ samplings eEMG are computed at a frequency $f_{\text{stim}}$, and then the muscle activations under every stimulation loop are obtained through normalization of

Fig 1. The architecture diagram of the hybrid FES system. The system contains two functionality parts: one is to control muscle activations with eEMG feedback and the other is to predict FES-induced torque based on eEMG.

Fig 2. Prediction of FES-induced ankle joint torque with eEMG for a single SCI patient.
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For joint torque estimation computations, the subject needed to be seated on the chair with the ankle at 90 degrees, while the joint center was aligned with the axis of a calibrated dynamometer. The shank was adjusted with the knee joint at 40 degrees. The foot was strapped to the pedal to transmit ankle torque to the dynamometer and to allow the optimal recording of isometric/non-isometric ankle torque. Raw eEMG of TA or MG muscle group and ankle joint torque were recorded, amplified (gain 1000) and sampled at a frequency $f_{\text{samp}} = 4096\text{Hz}$ through the Biopac amplifier and a 16-bit A/D national instrument card.

Results

FES-induced torque prediction with eEMG

The stimulation frequency $f_{\text{stim}}$ was set between 30 and 40Hz leading to the loop execution time between 25ms and 33ms. The suitable stimulation intensities were found to be from 20mA to 50mA specific to each patient. Then the stimulation intensity is fixed and PW modulation is performed to have different levels of muscle contractions to induce regular joint movement.

The test session included 2 phases: identification and prediction phases. Each sequence contained trapezoidal trains consisting of $2s$ stimulation (0.5s ramp up, 1s plateau and 0.5s ramp-down) and $2s$ rest. During identification phase that lasts between 33 and 40s, the plateau stimulation PW of each trapezoidal train was increased gradually with step size of from 40% to 100% of the maximum PW. After identification, the plateau stimulation PW was randomly determined within 50% to 100% of maximum PW in the prediction phase. The stimulation artifacts in the raw eEMG were removed by blanking with a window size at 10ms. Both the stimulus-activation model and activation-torque model are identified during the same identification phase. Fig. 2 shows the ankle joint torque prediction results based on RNN which was proposed for one SCI patient. Observed from the figure, we can see the joint torque prediction seems promising on the SCI patient, with root mean square error (RMSE) being 0.24Nm and variance accounted for (VAF) being 78.75% respectively.

Muscle Activation Control with eEMG

Afterwards, the model predictive controller is computing the PW level with PW-NMAV model updated at every stimulation loop and send the PW value to the wireless stimulator to perform the tracking control. Four different reference patterns of muscle activation under FES were tested and part of these results are presented: Every control loop is executed within 20ms, which does not exceed the maximum allowable time period for every stimulation loop $k$. In this paper, the desired muscle activation for the real-time control by FES is generated artificially following two patterns: 1) One kind of natural patterns with two continuous sinusoidal contraction for drop foot correction; 2) Actual muscle contraction pattern measured by EMG envelope from the able-bodied subject during a whole cycle of actual walking test. Fig. 3 shows the control results on one SCI patient, we could see from this figure that the muscle activation controlled by the FES controller can track the desired reference quite well.
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Discussion
This paper presents a hybrid FES system which can control muscle activation and predict joint torque with eEMG. Clinical experiment results on SCI subjects verify its feasibility and efficiency. Future work could be extended to applying such FES system on estimation/control issues of multiple muscles/joints with muscle/joint synergy considered, and comparison of M-wave during dynamic contractions and during isometric contractions is also worth investigating.

Authors’ Contributions
Zhan Li: Experiment preparation, data acquisition and processing, publication writing; David Guiraud: Experiment preparation, supervision of data processing and publication drafting, publication review; David Andreu: FES system implementation and technology support, publication review; Charles Fattal: Experiment preparation, medical support; Anthony Gelis: Experiment preparation, medical support; Mitsuhiro Hayashibe: Experiment preparation, data acquisition, supervision of data processing, publication review.

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Conflict of interest
The authors declare no conflict of interest.

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