Lanthanide-Doped Upconversion-Linked Immunosorbent Assay for the Sensitive Detection of Carbohydrate Antigen 19-9

Chaohui Zhou, Zhongyun Chu, Wenyue Hou and Xiuying Wang

Lanthanide-doped upconversion nanoparticles (UCNPs) have attracted considerable attention in detection of biological analytes and bioimaging owing to their superior optical properties, including high photochemical stability, sharp emission bandwidth, large anti-Stokes shifts, and low toxicity. In this work, we fabricated UCNP-linked immunosorbent assay (ULISA) for the sensitive detection of carbohydrate antigen 19-9 (CA19-9). The design is based on amino-functionalized SiO$_2$-coated Gd-doped NaYF$_4$:Yb$^{3+}$,Er$^{3+}$ upconversion nanoparticles (UCNPs@SiO$_2$-NH$_2$) as a direct background-free luminescent reporter; a secondary anti-IgG antibody (Ab$_2$) was conjugated to the surface of UCNPs@SiO$_2$-NH$_2$ (UCNP-Ab$_2$), and UCNP-Ab$_2$ was used for specific targeting of CA19-9. The UCNPs were well characterized by TEM, SEM, XRD, FT-IR, and UV-vis. The detection process was similar to enzyme-linked immunosorbent assay (ELISA). UCNPs were used as signal transducer to replace the color compounds for an enzyme-mediated signal amplification step. An anti-CA19-9 primary antibody (Ab$_1$) was fixed for capturing the CA19-9, and the fluorescence signal was obtained from the specific immunoreaction between UCNP-Ab$_2$ and CA19-9. Under optimum conditions, this ULISA shows sensitive detection of CA19-9 with a dynamic range of 5–2,000 U/ml. The ULISA system shows higher detection sensitivity and wider detection range compared with the traditional ELISA for CA19-9 detection. This strategy using UCNPs as signal transducer may pave a new avenue for the exploration of rare doped UCNPs in ELISA assay for clinical applications in the future.

Keywords: UCNPs, immunosorbent assay, cancer biomarker, CA19-9, immunodetection

INTRODUCTION

Cancer has been the leading cause of global death. Among various types of cancers, pancreatic cancer with extremely high mortality and poor prognosis is ranked the 4th leading cause of cancer death in the USA (Wolfgang et al., 2013; Siegel et al., 2019). In China, the incidence and mortality of pancreatic cancer are also increasing (Chen et al., 2016). The late diagnosis of cancers was deemed to be the leading cause of high mortality...
rate because of the lack of early symptoms and appropriate tools to
detect pancreatic cancer at an early stage. In order to decrease
mortality and improve survival of pancreatic cancer patient, it is
crucial to confirm the lesion at an early surgically resectable stage
(Qian et al., 2019). The CA19-9 has been widely used as a clinical
common tumor-specific biomarker for diagnosing pancreatic
cancer (Xu et al., 2019). CA19-9 is also the only approved
biomarker to guide and direct therapy, prognosis, and diagnostics
by the US Food and Drug Administration (FDA) (He et al., 2015).
Elevated levels (>37 U/ml) of CA19-9 are thought to be closely
related to pancreatic cancer (Wu et al., 2013). Thus, the accurate
monitoring of CA19-9 has been a vital tool for early diagnosis of
pancreatic cancers (Kaur et al., 2012; Singhi et al., 2019).

Enzyme-linked immunosorbent assay (ELISA) is an
extensively used immunological assay in medical diagnostic
for measuring the proteins, peptides, antibodies, haptons,
hormones, illegal drugs, cells, and their metabolites in biological
samples. ELISA presented a simple and reliable analytical
tool for the detection of target biological analytes (Kwong
et al., 2013). However, there are some limitations that hamper
its routine application in the clinical detection of cancer biomarkers due to the ELISA tests being mainly based on the
spectroscopic detection of a chromogenic substrate that yields
a measurable color product during the assay. This colorimetric
signal readout significantly affects the accurate detection of the
target biomolecules as the color intensity is proportional to the
concentration of target analytes. Unfortunately, the sensitivity
of colorimetric readout is relatively lower compared with
other signal readout such as fluorescence, which will decrease
the sensitivity of the traditional colorimetric ELISA assay.
Additionally, some color compounds in the biological samples
will also interfere with the color output (Acharya et al., 2013;
Tong et al., 2013; Xianyu et al., 2014; Gao et al., 2020).

Recently, nanoparticles (NPs) as signal amplifiers have been
widely used as strategies to improve the performance of the
traditional colorimetric output-based ELISA. Quantum dots,
fluorescent dye-doped polymer or silica NPs, catalytic NPs,
metal NPs, and magnetic NPs have been successfully used in
ELISA, remarkably improving the sensitivity of ELISA (Osterfeld
et al., 2008; Jans and Huo, 2012; Tong et al., 2013). Rare-earth
(RE)-doped upconversion luminescent nanoparticles (UCNPs)
as an optical background-free luminogens have exhibited
enormous potential in immunodetection owing to its possession
of large anti-Stokes shifts, high photochemical stability, long
photoluminescence (PL) lifetimes, and low toxicity (Wang and
Tanner, 2010; Liu et al., 2013; Zhao et al., 2013). UCNPs-based
linked immunosorbent assays have been designed for highly
sensitive detection of clinical biomarker such as cardiac troponin
I (Sirkka et al., 2016), multiple mRNAs (Hu et al., 2017), and
prostate-specific antigen (PSA) (Farka et al., 2017). However,
UCNP-based linked ELISA system for CA19-9 detection has not
been developed.

In this work, we developed a new UCNP-based linked
immunosorbent assay (ULISA) for the sensitive detection of
CA19-9. The system was constructed based on aminofunctionalized SiO₂-coated Gd-doped NaYF₄:Yb,Er UCNPs
(UCNPs@SiO₂) that works as signal transducer to provide the
fluorescence signal. UCNPs were coated with silica by inverse
deposition method and followed by functionalization with amino
groups on the surface (Hlaváček et al., 2014). Anti-mouse IgG
antibodies were conjugated to the surface of UCNPs@SiO₂-NH₂.
The strategy for detection of CA19-9 is illustrated in Scheme 1.
After optimizing testing condition, this ULISA could achieve
sensitive and rapid detection of CA19-9. This design strategy
of using UCNPs as the signal transducer to provide fluorescence
as an alternative output to color intensity will be extended to
wide-range applications in the area of immunodetection and
disease diagnosis.

**EXPERIMENTAL**

**Materials and Characterization**

All the applied chemicals such as Y₂O₃, Yb₂O₃, Er₂O₃, and
Gd₂O₃ in this work maintained high purity (purity ≥98%)
were provided by Sigma-Aldrich (USA) and without further
purification. Ammonium fluoride (NH₄F), absolute tetraethyl
orthosilicate (TEOS), and oleic acid (OA) were obtained from
Shanghai Reagent Company. The washing buffer (pH = 9.6)
employed in immunosorbent assay was doped with solution
components such as 50 mM NaH₂PO₄/Na₂HPO₄, 0.01% Tween
20, and 0.05% NaNO₃. All aqueous solutions in experiments were
prepared in distilled water (DIW, Millipore-Q, 18.2 MΩ).

The measurements of zeta potential were performed using
Malvern Zetasizer Nano ZS90; the morphology and size of
nanoparticles were characterized on a transmission electron
microscopy (TEM, JEOLE-2100) and field emission scanning
electron microscope (FESEM, LEOM530). Meanwhile, UV-visible
(UV-vis) absorption spectra were recorded on a Varian Cary-
Eclipse 500 apparatus. Nicolet 380 spectrometer system was
applied to record Fourier transform infrared (FT-IR) spectra.

**Preparation of UCNPs-SiO₂-NH₂**

The nanostructured UCNPs-SiO₂-NH₂ was fabricated in the
following procedures:

1. Synthesis of lanthanide-doped UCNPs (Hou et al., 2015).

   In the first step, a volume of 20 ml of ethanol and 30 ml of
OA solution were added to the beaker. Subsequently, 5 ml of
DIW and NaOH (1.2 g) were added under a steady magnetic
stirring rate to obtain a transparent color. Immediately,
3.2 ml of NH₄F was added to the above system. After stirring for 10 min, a certain amount
of RECl₃ solution (0.4 M, 4 ml) was gradually dropped. It
should be noted that RE referred to the mixture of the
above rare earth elements, and the ratio of the amount of
the substance was Y:Gd:Yb:Er = 9:30:10:1. After stirring for
30 min, the dispersion was completely transferred to a
hydrothermal reaction vessel with hydrothermal treatment
at 180°C going on for 2 h, and the upper layers and the lower
sample nanoparticles were carefully separated and dissolved
in cyclohexane, followed by aspiration with absolute ethanol
before centrifugation. All of the nanomaterials were rinsed
repeatedly with water and ethanol for several cycles to
remove unreacted precursor and then subjected to a freeze-drying process overnight.

(2) The silica coating on UCNPS (UCNPs@SiO$_2$). The reverse microemulsion method was used to achieve the purpose of encapsulating UCNPs (Hlaváˇcek et al., 2014). The specific route was to mix 2-(2-[4-(1,1,3,3-tetramethylbutyl) phenoxy] ethoxy) ethanol (Triton X-100), n-hexyl alcohol, and cyclohexane in a ratio of 4:1:1 and adding a certain amount of DIW to form a transparent and stable microemulsion system. Then, nanoparticles were thrown into the system, dispersed, and pipetted into the flask for vigorous magnetic stirring. Afterwards, a portion of concentrated ammonia water was taken and added dropwise; when it was uniformly dispersed, TEOS was continuously placed into the system under continuous stirring for 10 h. Standing aging and subsequent ethanol washing and preservation steps were expected.

(3) Surface amino functionalization of UCNPs (UCNPs@SiO$_2$-NH$_2$). A mixture of methanol and glycerol in a volume ratio of 5:3 was used to disperse the UCNPs@SiO$_2$ with magnetic stirred at 65°C. Afterwards, 10 ml of aminopropyltriethoxysilane (APTES, Sigma-Aldrich) was added for 5 h of continuous reaction; the nanocomposites were washed with ethanol and phosphate buffer solution (PBS, pH = 7.4) for three times.

Conjugation of UCNPs@SiO$_2$-NH$_2$ and Secondary Antibody

The UCNPs-SiO$_2$-NH$_2$ were conjugated to a secondary antibody via standard EDC/sulfo-chemistry (Ko and Lim, 2014). In a typical synthesis, the presynthesized UCNPs@SiO$_2$-NH$_2$ were dispersed in 10 ml of PBS solution at room temperature under slight magnetic stirring for 2 h. Then, 1-ethyl-3-(dimethylaminopropyl) carbodiimide (EDC) and N-hydroxysuccinimide (NHS) mixture (1:1) were added and mixed for 1 h. The secondary antibody (Ab$_2$, Abcam) was introduced into the system and kept going for another 2 h under regular shaking. The prepared sample UCNPs@SiO$_2$-Ab$_2$ was finely purified by multiple centrifugation to remove unreacted solvents or impurities, then the complex was dispersed in PBS for next experiments.

UCNP-Based Linked Immunosorbent Assay

First, the optimal coating concentration of monoclonal antibodies was determined using a transparent and clean 96-well plate with pretty protein binding capacity (Corning, Germany). Based on the concentration test, each well in plate was coated with primary antibodies (Ab$_1$, Abcam) at an optimal concentration of 2 µg/ml for overnight (4°C), except for this, all subsequent procedures were launched under room temperature. Subsequently, the plate was rinsed with 250 µl of washing buffer four times manually. Naturally, the remaining free sites on the plate were blocked with 1% BSA solution (PBS, pH = 7.4) for 2 h. After washing procedures, the standard CA19-9 solution (100 µl) with various concentrations was added to each well and incubated for 2 h. Similarly, the unbound Ab$_1$ was rinsed off with PBS buffer. Immediately, UCNPs@SiO$_2$-Ab$_2$ was introduced into each well and further incubated for 2 h and following by washing. Finally, the upconversion luminescence signals were recorded under a custom-built upconversion microplate reader equipped with a 980-nm laser transmitter.

RESULTS AND DISCUSSION

Characterization and Surface Modification of UCNPs

The application of ULISA for detection strongly relies on the performance of the luminescent reporter. Among the various developed upconversion materials, NaYF$_4$:Yb/Er nanoparticles with hexagonal crystal structure express greater upconversion efficiency than its cubic crystal form. Moreover, the dispersibility and stability of nanomaterials are also key factors in the assay. In our study, the as-prepared UCNPs with oleic acid as a stabilizer were coated with silica shell, which not only enhance
the dispersion of UCNPs but also provide a large number of sites for subsequent functional modification.

As shown in Figure 1, the hexagonal phase structure of UCNPs was clearly shown in the FESEM image (Figures 1A,B). Furthermore, both the TEM image (Figure 1C) and the FESEM images verified the good dispersibility of the nanoparticles. Additionally, it has uniform size distribution with a homogeneous diameter of 48.6 ± 4.9 nm (Figure 1E). Notably, UCNPs also emerge as a considerable degree of crystallinity and sharpness. The selected-area electron diffraction pattern (Figure 1D) exhibited a single crystal diffraction ring, which is in accordance with the X-ray diffraction results. The corresponding conspicuous peak diffraction (Figure 1F) such as the angles of 17.08°, 29.85°, 30.42°, 43.24°, and 53.75° corresponds to the planes of (100), (110), (101), (201), and (102), respectively, suggesting the pure hexagonal phase of UCNPs. For upconversion materials, the luminescence properties of UCNPs in ULISA applications must be taken into consideration. Under the irradiation with laser at 980 nm, the upconversion luminescence spectrum is recorded in Supplementary Figure 1. The three emission peaks at about 520, 540, and 660 nm were observed, and the most intensive
fluorescence is centered at 540 nm, which could be ascribed to the typical green region. The full UV spectrum of UCNPs is shown in Supplementary Figure 2. In order to improve water dispersibility and stability of UCNPs, the one-step silica-coating protocol was conducted using the reverse microemulsion method. In the previous exploration process, the one-step silicon coating easily lead to agglomeration of UCNPs, a two-step protocol was used to prepare a more stable and compact silica shell. Figures 1G,H shows the TEM image of the silica-coated UCNPs. It was clear that each nanoparticle was coated with about 5 nm compact silica shell.

In order to facilitate the coupling of UCNPs to Ab2, the amino functional modification of the surface was conducted. In the first step, the potential trend (Supplementary Figure 3) in different modification stages was measured. Owing to hydroxyl groups on the surface of the silica coating, it displayed a potential change from positive (+36.2 mV) to negative (−31.7 mV). However, after modification with APTES, the potential changed to +33.2 mV, which could account for the amino group of the surface of the silica. Thus, this result demonstrated that amino was successfully conjugated to the surface of UCNPs@SiO2. Additional characterization was further conducted to verify the successful modification. By means of FT-IR spectroscopy (Figure 2), the bands at 1,094 and 3,420 cm$^{-1}$ are assigned to stretching vibrations of −Si–O–Si and O–H in UCNPs@SiO2; this fully confirmed the successful wrapping of silica. In the nanocomplex UCNPs@SiO2-NH2, the characteristic absorption bands of N–H (1,641 cm$^{-1}$) bending vibrations and C–H (2,974 cm$^{-1}$) stretching vibrations indicate the existence of amino group (Huang et al., 2010). The successful coating of SiO2-NH2 onto the surface of UCNPs not only enables the dispersibility of UCNPs in biological fluids but also provides a lot of attachment sites for subsequent protein conjugation steps.

**Conjugation of UCNPs@SiO2-NH2 and Ab2**
The Ab2 were conjugated to the surface of UCNPs@SiO2-NH2 through a standard EDC/NHS strategy. The UV-vis spectroscopy was used to characterize the conjugation of UCNPs@SiO2-NH2 and Ab2 (Figure 3). The characteristic absorption peak of Ab2 was observed at 280 nm, which is comparable with the no obvious absorption peak of the UCNPs@SiO2-NH2. After conjugation of Ab2 to the surface of UCNPs@SiO2-NH2, the absorption peak at 280 nm was observed and the intensity of absorption band increased with the concentration of conjugated Ab2. The results indicated that Ab2 was successfully conjugated to the surface of UCNPs@SiO2-NH2.

**Optimization of Concentration of Ab1**
The coating of the antibody on the plate is based on the physical adsorption of the protein by polystyrene plastic. The amount of antibody coated on the experimental plate directly determines the detection limit of this experiment, which has
a great impact on the results. Therefore, it is necessary to determine the optimal concentration of Ab₁. In detail, firstly, the different concentrations of Ab₁ (0.5, 1, 1.5, 2, 4, and 8 µg/ml) were immobilized in plate; subsequently, the excess horseradish peroxidase (HRP)-labeled Ab₂ were added and incubated, and TMB substrate solution was added to the microwell plate after washing off the unreacted HRP-labeled Ab₂. The absorbance of the reaction solution was monitored as shown in Figure 4, with the increase of the concentration of Ab₁, the absorbance gradually increased and the absorbance value reached a maximum at the concentration of 2 µg/ml. As the concentration continued to increase, the absorbance value gradually reduced, implying that there is the largest Ab₁ adsorption capacity when the concentration of Ab₁ reached 2 µg/ml. Therefore, 2 µg/ml was used as the optimal concentration of Ab₁ in the following study.

**Sensitivity of the UCNP-Based Linked Immunosorbent Assay**

The detection of CA19-9 with ULISA was conducted similarly as traditional ELISA. Only a UCNP-Ab₂ was used as a direct luminescent reporter to replace the color compounds for enzyme-mediated color generation. Under optimum conditions, the standard concentration of CA19-9 from 5 to 2,000 U/ml were prepared via serial dilution in PBS, and then this ULISA system was used for the quantitative assay. The detection results for CA19-9 are shown in Figure 5A. The fluorescence intensity of UCNPs gradually increased along with the concentration of CA19-9 from 5 to 2,000 U/ml. A linear relationship between the fluorescence intensity of UCNPs at 540 nm and concentration of CA19-9 from 5 to 2,000 U/ml was obtained; the linear range for the quantitative assay is shown in Figure 5B. The correlation equation can be calculated as $y = 0.124x + 115.56$, and a correlation coefficient ($R^2$) of 0.9959 was obtained. Compared with conventional ELISA assay for CA19-9 detection, this ULISA system shows a sensitive detection of CA19-9 with a dynamic range of 5–2,000 U/ml. The ULISA system shows higher detection sensitivity and wider detection range compared with traditional ELISA for the detection of CA19-9. This strategy using UCNPs as signal transducer may pave a new avenue for the exploration of rare doped UCNPs in ELISA assay for clinical applications in the future.
**SUPPLEMENTARY MATERIAL**

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fchem.2020.592445/full##supplementary-material

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**Supplementary Figure 1** | Luminescence spectroscopic characterization of UCNPs upon NIR excitation at 980 nm.

**Supplementary Figure 2** | The full UV spectrum of UCNPs.

**Supplementary Figure 3** | Zeta potentials of UCNPs, UCNPs@SiO2, and UCNPs@SiO2-NH2.

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**Conflict of Interest:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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