Measures of spike train synchrony for data with multiple time scales

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**HIGHLIGHTS**

- Adaptive generalizations to ISI-distance, SPIKE-distance and SPIKE-synchronization.
- Generalizations disregard spike time differences not relevant on a more global scale.
- Rate-independent extension RIA-SPIKE-distance focuses specifically on spike timing.
- Correction of edge effects and treatment of special cases.

**ABSTRACT**

**Background:** Measures of spike train synchrony are widely used in both experimental and computational neuroscience. Time-scale independent and parameter-free measures, such as the ISI-distance, the SPIKE-distance and SPIKE-synchronization, are preferable to time scale parametric measures, since by adapting to the local firing rate they take into account all the time scales of a given dataset.

**New method:** In data containing multiple time scales (e.g. regular spiking and bursts) one is typically less interested in the smallest time scales and a more adaptive approach is needed. Here we propose the A-ISI-distance, the A-SPIKE-distance and A-SPIKE-synchronization, which generalize the original measures by considering the local relative to the global time scales. For the A-SPIKE-distance we also introduce a rate-independent extension called the RIA-SPIKE-distance, which focuses specifically on spike timing.

**Results:** The adaptive generalizations A-ISI-distance and A-SPIKE-distance allow to disregard spike time differences that are not relevant on a more global scale. A-SPIKE-synchronization does not any longer demand an unrealistically high accuracy for spike doublets and coinciding bursts. Finally, the RIA-SPIKE-distance proves to be independent of rate ratios between spike trains.

**Comparison with existing methods:** We find that compared to the original versions the A-ISI-distance and the A-SPIKE-distance yield improvements for spike trains containing different time scales without exhibiting any unwanted side effects in other examples. A-SPIKE-synchronization matches spikes more efficiently than SPIKE-synchronization.

**Conclusions:** With these proposals we have completed the picture, since we now provide adaptive generalized measures that are sensitive to firing rate only (A-ISI-distance), to timing only (A-ARI-SPIKE-distance), and to both at the same time (A-SPIKE-distance).

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1. Introduction

In neuroscience the neuronal action potential and its complex molecular behavior (Bear et al., 2007) is often reduced to time-discrete events called spikes. Due to the all-or-nothing paradigm of neurons together with the long silent periods, the time stamps of the spike events are considered to be an accurate enough descrip-
tion of the neuronal membrane potential (Quian Quiroga and Panzeri, 2013). These sequences of consecutive spikes are called spike trains. While spike trains do not directly provide information about the connections between neurons, some form of link between two neurons is often inferred by the similarity of their spike trains. A spike train distance does not take into account the specific type of linkage, but simply quantifies how (dis)similar the two spike trains are. This makes spike train distances universal and as such they can be applied to all systems that can be reduced to point processes. In addition to the obvious neuroscience applications, they have already been used to study inter-personal coordination (Rabinowitch and Knafo-Noam, 2015) and social cognition (Zapata-Fonseca et al., 2016) among many other fields.

Over the years many different measures have been developed in order to quantify similarities between two or more spike trains (see Victor, 2015; Naud et al., 2011; Kreuz, 2011 for an overview). The two most known time scale parametric measures, the Victor–Purpura (Victor and Purpura, 1996) and the van Rossum distance (van Rossum, 2001), describe spike train (dis)similarity based on user-defined time scales to which the measures are mainly sensitive. One drawback of these measures is the fixed time scale, since it sets a boundary between rate and time coding for the whole recording. However, for real data which typically contain many time scales (such as regular spiking and bursts), this is difficult to detect with a measure that is mainly sensitive to only one of them (Chicharro et al., 2011).

The problem of having to choose one time scale has been eliminated in the three time-resolved and time scale independent measures ISI-distance (Kreuz et al., 2007, 2009), SPIKE-distance (Kreuz et al., 2011, 2013) and SPIKE-synchronization (Kreuz et al., 2015). The ISI-distance (Kreuz et al., 2007) is a measure of instantaneous rate dissimilarity. It uses the interspike intervals (ISIs) to estimate the local firing rate of spike trains and quantifies their differences in a time-resolved manner. The SPIKE-distance (Kreuz et al., 2011) compares the spike time accuracy between spike trains and uses instantaneous firing rates to adapt to the local time scale. Finally, SPIKE-synchronization (Kreuz et al., 2015) is a discrete time-resolved measure of similarity based on ISI-derived coincidence windows that are used to determine if two spikes from different spike trains are coincident or not. These measures have already been successfully applied in many different contexts; for example they have been used to detect determinism in point processes (Andrzejak et al., 2014), to find correlations between spike trains and behavior in an inverse neurocontroller (Dura-Bernal et al., 2016) and to evaluate a bio-inspired locomotion system in robotics (Espinol et al., 2016).

Since they always adapt to the local firing rate, all three of these measures are time scale free. While they correctly identify the relative firing rate differences, they have no concept of actual time scales and treat all time scales as equally important. This has the consequence that for very small time scales even minor deviations from perfect synchrony lead to very high values of dissimilarity. However, for real data the smallest time scales are often not very relevant and any dissimilarities there can mostly be disregarded. Thus in this case the measures’ focus on the local time scales results in a (spurious) amplification of dissimilarities which compared to the global time scales are rather negligible.

Here we address this problem by proposing generalizations to the three measures called adaptive ISI-distance (A-ISI-distance), adaptive SPIKE-distance (A-SPIKE-distance) and adaptive SPIKE-synchronization (A-SPIKE-synchronization). These generalized definitions add a notion of the relative importance of local differences compared to the global time scales. In particular, they start to gradually ignore differences between spike trains for ISIs that are smaller than a minimum relevant time scale (MRTS). The MRTS is implemented by an additional variable $T$ which can either be defined as a parameter or estimated directly from the data.

In some neuroscience applications only the similarity of spike timing is important and rate differentiation is not a desired property. While the A-ISI-distance is sensitive to firing rate alone and the A-SPIKE-distance responds to differences in both rate and timing, there is currently no measure that focuses only on spike timing. Therefore, in a second step we extend the A-SPIKE-distance into the rate-independent adaptive SPIKE-distance (RIA-SPIKE-distance) which still identifies spike time differences but ignores any rate deviations between the spike trains.

The remainder of this paper is organized as follows. In Section 2 we describe the generalized definitions of the three measures, the A-ISI-distance (Section 2.1), the A-SPIKE-distance (Section 2.2), and A-SPIKE-synchronization (Section 2.3). In Section 2.4 we introduce a way to estimate the threshold value directly from the data. We then investigate using both simulated and real data how both the original measures and the adaptive generalizations deal with multiple time scales (Section 2.5). In Section 3 we add a rate-independent extension to A-SPIKE-distance (Section 3.1) and afterwards study the effects of the extension (Section 3.2). The implications of the extensions are discussed in Section 4. Finally, in Appendix A we cover some non-trivial subtleties of the definitions for all three measures. First we provide the definitions for the periods before the first and after the last spike in a spike train (where the interspike interval is not defined), and then we deal with the two special cases of empty spike trains and spike trains with only one spike. The two experimental datasets used in Section 2.5 are described in Appendix B.

2. Adaptive generalizations

In this section we introduce the adaptive generalizations of the established measures ISI-distance (Kreuz et al., 2007), SPIKE-distance (Kreuz et al., 2011) and SPIKE-synchronization (Kreuz et al., 2015), which we will call A-ISI-distance, A-SPIKE-distance, and A-SPIKE-synchronization. All three generalizations are built on a minimum relevant time scale (MRTS) which is implemented via the threshold parameter $T$. This threshold is used to determine if a difference between the spike trains should be assessed in a local context or in relation to the global time scales. This threshold is used for all three measures, but the way it is applied varies. The generalized measures fall back on the original definitions when $T = 0$. In the following this is what we refer to whenever we talk of the original measures. In this case even the smallest time scales matter and all differences are assessed in relation to the local context only.

Note that the upcoming definitions only apply to the interval between the first and the last spike. In Appendices A.1 and A.2 they will be completed to range from the start of the recording $t_c$ to the end of the recording $t_e$.

2.1. Adaptive ISI-distance

The A-ISI-distance measures the instantaneous rate difference between spike trains (see Fig. 1A). It relies on a time-resolved profile, meaning that a dissimilarity value is defined for each time instant. To obtain the profile, we assign to each time instant $t$ the time of the previous spike

$$T^{(n)}_p(t) = \max(t^{(n)}_i | t^{(n)}_i \leq t) \text{ for } t^{(n)}_i \leq t \leq t^{(n)}_{M_t}$$

(1)
order to assess the accuracy of spike events, each spike is assigned the distance to its nearest neighbor in the other spike train
\[
\Delta t_i^{[n]} = \min_j (|t_i^{[n]} - t_j^{[m]}|).
\] (7)

These distances are then interpolated between spikes using for all times \( t \) the time differences to the previous spike
\[
x_p^{(n)}(t) = t - t_i^{(n)} \quad \text{for} \quad t_i^{(n)} \leq t < t_i^{(n+1)},
\] (8)
and to the following spike
\[
x_p^{(n)}(t) = t_{i+1}^{(n)} - t \quad \text{for} \quad t_i^{(n)} \leq t < t_{i+1}^{(n+1)}.
\] (9)

These two quantities define a time-resolved dissimilarity profile from discrete values the same way as Eqs. (1) and (2) did for the A-ISI-distance. The instantaneous weighted spike time difference for a spike train can then be calculated as the interpolation from one difference to the next
\[
S_n(t) = \frac{\Delta t_i^{(n)}(t) x_p^{(n)}(t) + \Delta t_{i+1}^{(n)}(t) x_p^{(n)}(t)}{x_{ISI}^{(n)}(t)}, \quad t_i^{(n)} \leq t < t_{i+1}^{(n+1)}.
\] (10)

This function is analogous to the term \( x_{ISI}^{(n)} \) for the ISI-distance, with the only difference that it is piecewise linear instead of piecewise constant. It is also continuous.

The pairwise A-SPIKE-distance profile is obtained by averaging the weighted spike time differences, normalizing to the local firing rate average and, finally, weighting each profile by the instantaneous firing rates of the two spike trains
\[
S_{m,n}^{A}(t) = \frac{S_n x_{ISI}^{m}(t) + S_m x_{ISI}^{n}(t)}{2|x_{ISI}^{(m)}(t)| \max|x_{ISI}^{(n)}(t)|, |t|}.
\] (11)

We define the MRTS by using a threshold, that replaces the denominator of weighting to spike time differences if the mean is smaller than the threshold \( T \). This profile is analogous to the pairwise A-ISI-profile \( I_{m,n}^{A}(t) \), but again it is piecewise linear, not piecewise constant. Unlike \( S_n(t) \) it is not continuous, since typically it exhibits instantaneous jumps at the times of the spikes. The multivariate A-SPIKE-profile is obtained the same way as the multivariate A-ISI-profile, by averaging over all pairwise profiles
\[
S_A(t) = \frac{1}{N(N-1)} \sum_{m=1}^{N-1} \sum_{n=m+1}^{N} S_{m,n}^{A}(t).
\] (12)

Finally, also the A-SPIKE-distance is calculated as the time integral over the multivariate profile
\[
D_A = \frac{1}{T^T - T} \int_{t_i}^{t_i^T} S_A(t) dt.
\] (13)

For \( T = 0 \) also the A-SPIKE-distance falls back to the SPIKE-distance.

The effect of applying the threshold can be seen in Fig. 2. The first event of five spikes is compressed more and more until it becomes a single burst in the fourth event. The original SPIKE-distance profile \( S(T) \) has the same proportions of dissimilarity for all events, since it uses local context only and thus considers all time scales as equal, while the A-SPIKE-distance profile \( S_A(t) \) is scaled down when the differences become small compared to the global time scales.

2.3. Adaptive SPIKE-synchronization

A-SPIKE-synchronization quantifies how many of the possible spike coincidences in a dataset are actually occurring (Fig. 1C). While the A-ISI-distance and the A-SPIKE-distance are measures of dissimilarity which obtain low values for similar spike trains, A-SPIKE-synchronization measures similarity. If all the spikes are coincident with a spike in all the other spike trains, its value will be one. In contrast, if none of the spikes are coincident, it will be zero.
The original SPIKE-synchronization (Kreuz et al., 2015) is parameter- and time scale-free, since it uses the adaptive coincidence detection first proposed for the measure event synchronization (Quian Quiroga et al., 2002). The coincidence window, i.e., the time lag below which two spikes from different spike trains, \( t_i^{(n)} \) and \( t_j^{(m)} \), are considered to be coincident, is adapted to the local firing rate. Spikes are coincident only if they both lie in each other’s coincidence windows.

For A-SPIKE-synchronization we generalize the definition by introducing a threshold, which decides if the window is determined locally or if the global time scales should be taken into account. As a first step, we define the ISI before the spike as

\[
\tau_i^{(n)} = \lim_{t \to t_i^-} x_i^{(n)}(t)
\]

and the ISI after the spike as

\[
\tau_i^{(n)} = \lim_{t \to t_i^+} x_i^{(n)}(t).
\]

The coincidence window for spike \( i \) of spike train \( n \) is defined by determining the minimum coincidence window size for a spike as half the length of the two ISIs adjacent to the spike

\[
\tau_i^{(n)} = \frac{1}{2} \min(\tau_i^{(n)} - \tau_i^{(n)}),
\]

and allowing asymmetric coincidence windows based on MRTS. This is done by replacing \( \tau_i^{(n)} \) with the threshold value \( T \), if it is the smaller of the two. Since the threshold value is derived from ISIs and the coincidence window spans both sides of the spike, only half of the threshold spans each side. For the A-ISI- and the A-SPIKE-distance the changes induced by the threshold appear gradually, but for A-SPIKE-synchronization they occur as an abrupt jump from 0 to 1. Therefore, to compensate for the binary nature of A-SPIKE-synchronization, the threshold is divided by two, resulting in an overall factor of 1/4. The coincidence windows of neighboring spikes are not allowed to overlap, and thus each side is limited to half the ISI even if the threshold is larger. Thus, the coincidence window before the spike is determined as

\[
\tau_i^{(n)} = \min \left\{ \frac{1}{4} T, \frac{1}{2} \tau_i^{(n)} \right\},
\]

and the coincidence window after the spike as

\[
\tau_i^{(n)} = \min \left\{ \frac{1}{4} T, \frac{1}{2} \frac{1}{T_i^{(n)}} \right\}.
\]

The combined coincidence window for spikes \( i \) and \( j \) is then defined as

\[
\tau_{ij}^{(n,m)} = \begin{cases} \min(\tau_i^{(n)}, \tau_j^{(m)}) & \text{if } t_i \leq t_j \\ \min(\tau_i^{(n)}, \tau_j^{(m)}) & \text{otherwise} \end{cases}.
\]

The coincidence criterion can be quantified by means of a coincidence indicator

\[
C_i^{(n,m)} = \begin{cases} 1 & \text{if } \min_j |(t_i^{(n)} - t_j^{(m)})| < \frac{\tau_{ij}^{(n,m)}}{\tau_i^{(n)}} \\ 0 & \text{otherwise} \end{cases}
\]

This definition ensures that each spike can only be coincident with at most one spike in the other spike train. The coincidence criterion assigns either a one or a zero to each spike depending on whether it is part of a coincidence or not. For each spike of every spike train, a normalized coincidence counter

\[
C_i^{(n,m)} = \frac{1}{N - 1} \sum_{m \neq n} C_i^{(n,m)}
\]

is obtained by averaging over all \( N - 1 \) bivariate coincidence indicators involving the spike \( i \) in spike train \( n \).

This way we have defined a coincidence indicator for each individual spike in the spike trains. In order to obtain one combined similarity profile, we pool the spikes of the spike trains as well as their coincidence indicators by introducing one overall spike index \( k \). This yields one pooled set of coincidence indicators

\[
|C_k| = \bigcup_n |C_i^{(n,m)}|
\]

from which the A-SPIKE-synchronization profile \( C_k(t_k) \) can be obtained via \( C_k(t_k) = C(k) \). Finally, A-SPIKE-synchronization is defined as the average value of this discrete profile

\[
S_k = \frac{1}{M} \sum_{k=1}^{M} C_k(t_k),
\]

where \( M \) is the overall number of spikes. In Fig. 3 we illustrate how the asymmetric coincidence windows of A-SPIKE-synchronization allow for a better coverage of burst events which makes it easier to match spikes when compared to the original SPIKE-synchronization (A-SPIKE-synchronization with \( T = 0 \)). It is important to note that reducing differences below threshold adds coincidences and thus, since it is a measure of similarity, A-SPIKE-synchronization can only increase.

2.4. Selecting the threshold value

In neuroscience typical time scales are in the range of milliseconds or sometimes seconds and any time scales below this will not be considered relevant. In fields such as meteorology the respective time scales could be hours and days or even months and years. The relevant time scales clearly depend on the system under consideration. Setting the minimum relevant time scale (MRTS) for a given dataset might not be a simple task. To address this, we propose a method to extract a threshold value from the spike trains, that is based on the proportions of the different time scales present in the data.

It is important to note that the selected MRTS is not an indicator of a time scale of the system; it just determines the outcome of the
adaptive generalizations. It is also not a hard set limiter neglecting everything below the threshold, but rather it marks the time scale from which on differences are considered in the global instead of the local context. Thus from this time scale on deviations from synchrony are treated as less and less relevant the smaller they get, even if they are large in relation to the local time scales.

The purpose of the threshold is to act as an indicator of what globally is a high rate or inversely a small ISI. The original normalizations are based on the ISIs, so it is reasonable to determine the threshold from the pooled ISI-distribution. We use the ISIs after the edge effect has been corrected (see Appendix A.1). The threshold should fulfill two main criteria. First, it needs to increase proportionally to the spike count, so that increasing rates (or longer recordings with the same rate) do not change the threshold. Second, the threshold should respond to changes in the ISI-distribution so that it is able to adapt between single and multiple time scale datasets. In Fig. 4 we use a simple spike train motif of just four spikes to illustrate these two criteria.

The most straightforward threshold would be the mean length of the ISIs

\[
(L_{ISI}) = \frac{\sum_{g=1}^{G} t_{ISI}^{g}}{M_{ISI}} = \frac{L}{M_{ISI}}.
\]

Here \(t_{ISI}^{g}\) denotes the ISI-length and \(M_{ISI}\) is the total number of ISIs in the pooled ISI-distribution. In the numerator the sum of the lengths of all ISI equals the overall length \(L\) of the pooled ISIs. Apart from edge effect corrections this is equal to the product of recording length and number of spike trains which is a constant. Thus while the mean of ISIs depends on the number of spikes (Fig. 4A), for a given number of spikes (number of ISIs) it is completely independent of how the ISIs are distributed around the mean (Fig. 4B). It adapts to the spike count but not to the proportions in which the ISIs appear in the data thus fulfilling the first but not the second criterion.

To fulfill both criteria one needs to not just count the interspike intervals but weight them by their length. This reduces the importance of short ISIs and allows the long ISIs to influence the threshold accordingly and not just number. It is equivalent to taking the mean of the second moments of the ISIs

\[
T = \sqrt{\langle (L_{ISI})^2 \rangle} = \sqrt{\frac{\sum_{g=1}^{G} t_{ISI}^{g}^2}{M_{ISI}}}, \tag{25}
\]

Note that in order to obtain a value with the right dimension the square root of the average must be taken. This threshold value has roughly the same dependence on the number of spikes as the mean value (Fig. 4A), however, in contrast to the mean it also sensitive to changes in the ISI-distribution. In summary, using \(T\) as the MKTS fulfills both criteria set for the threshold.

2.5. Results

In this section we investigate how both the adaptive generalizations (with automated thresholding) and the original measures deal with multiple time scales. For the A-ISI-distance and the A-SPIKE-distance we use a test spike train set consisting of simulated and real spike trains to study the effect of the generalized versions (Section 2.5.1). After that, in Section 2.5.2, we study on real MEA recordings how A-SPIKE-synchronization differs from SPIKE-synchronization. In Section 2.5.3 we systematically test the influence of the amount of bursts on the difference between adaptive and original measures. Finally, in Section 2.5.4 we investigate how the adaptive versions change the analysis of neuronal reliability in an experimental dataset.

2.5.1. Adaptive ISI-distance and adaptive SPIKE-distance

We address two points. First, we look at the sensitivity of the adaptive generalizations and verify that in the presence of bursts they perform better than the original measures. Second, we also make sure that the changes are specific, e.g., we confirm that in all other cases and especially if there are no bursts, the adaptive generalizations do not exhibit unwanted side effects.

To this aim, we use a test set composed of both artificial and real spike trains (Fig. 5) to compare A-ISI-distance to ISI-distance and A-SPIKE-distance to SPIKE-distance. We use two models to generate
our samples. For the spike trains with perfect periodicity we use a
time varying steady rate (fixed ISI) model. For samples with more
variability in spike timing we used a Poisson spiking model, where
the rate is fixed for a certain window at a time. In some cases we
add small jitter noise to both models. The artificial spike trains
1–25 are designed to exhibit a variety of stereotypical spiking behaviors
including both single and multiple time scales. The experimental
spike trains 26–30 consist of short recordings from neuronal cultures
on micro electrode arrays (see Appendix B.1 for details). For
the adaptive versions the threshold is estimated from the data (see
Section 2.4) for each pair separately.

In the analysis every spike train is paired with all the others.
Because for both the A-ISI-distance and the A-SPIKE-distance the
MRTS 7 can only reduce but never increase the dissimilarity value,
all pairs are found in the lower half of the scatter plot (Fig. 6).
Furthermore, all values between pairs of spike trains are close to or
on the diagonal, which means that both versions attain very similar
values or even the same value. The differences between the two
SPIKE-distances are slightly more pronounced than the differences
between the two ISI-distances. Such seemingly small differences can
still be of high significance since in a typical experimental setup it
is rarely the absolute value of similarity that matters but rather
the relative order of similarity for different conditions. Moreover,
in real data the range of similarity values obtained is usually
quite small which further increases the relative importance of small
changes in similarity.

For one spike train at a time we then look at all its pairings and sort
the results in ascending order according to the original versions. The results from the adaptive versions are arranged in
the same order. If the order of the spike train pairs does not match,
there is a clear difference in the way the two measures consider
spike train similarity.

We now investigate in more detail not only the largest absolute,
but also the largest relative changes observed in Fig. 7. First, the
largest absolute changes are identified by calculating the Euclidean
distances between the results for the two spike train pairs. They
typically take place for pairs of spike trains with large distances.
Next, since deviations from near perfect synchrony are more promi-

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**Fig. 5.** Spike train test set used to compare the generalized vs. the original measures
of spike train synchrony. Spike trains 1–25 are artificially constructed examples
which cover a range of archetypical spiking patterns, whereas spike trains 26–30
are selected examples of neuronal spiking data from a neuronal culture recorded on
a micro electrode array (see Appendix B.1). All spike trains are normalized by their
total length.

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A-ISI-distance or SPIKE- and A-SPIKE-distance average. For both
distances they mostly occur for pairs of very similar spike trains.

For the A-ISI-distance, the spike train pairs showing the largest
absolute change compared to the ISI-distance can be seen in Fig. 7A.
The two measures show a different order of similarity: while the
ISI-distance increases, the A-ISI-distance decreases from the first
to the second pair. Spike trains 27 and 30 in the first pair are seen
very similarly (deviation <1%) by both measures. However, when
spike train 27 is paired with spike train 9, the ISI-distance con-
siders the local time scale only and thus has unreasonably high
demands on the spikes of the burst in spike train 27 which leads to
large fluctuations in similarity. For the A-ISI-distance on the other
hand the burst matches another event with relatively high rate and
treats this event as a coinciding burst. Outside of the burst the two
measures agree that the spike trains are very dissimilar.

Fig. 7B depicts the two spike train pairs exhibiting the largest
relative change between the two ISI-distances. While the first pair
is seen as relatively similarly (deviation <5%), the main difference is
found for the second spike train pair. Here the ISI-distance looks at
the detailed structure and judges the interspike intervals within the
bursts as very dissimilar, whereas the A-ISI-distance sees simply
matching bursts and attains a considerably lower distance value
than the ISI-distance (0.100 vs. 0.129).

For the A-SPIKE-distance, the pairs of spike trains showing
the largest absolute change compared to the SPIKE-distance are
depicted in Fig. 7C. As there are no bursts in either of the two spike

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2.5.2. Adaptive SPIKE-synchronization

A-SPIKE-synchronization cannot be meaningfully tested by
using the spike train set of Fig. 5. The perfect periodicity in
many spike trains makes analysis of the A-ISI-distance and the
A-SPIKE-distance simple, but causes very abrupt changes in A-
SPIKE-synchronization due to its binary nature. The values can be
computed, but the largest differences are not meaningful with this
dataset, since many spike trains with bursts jump from zero to a
large value and there is no way of ordering different pairs hav-
ing zeros in the original measure. Thus, we here use a qualitative
approach together with insights from the analysis of A-ISI-distance
and A-SPIKE-distance.

As a side effect of being time scale adaptive, SPIKE-
synchronization demands very high spike timing accuracy during
fast firing. This leads to situations such as the one shown in Fig. 3
(Section 2.3). For spike trains 3 and 4 the spikes in the first event
are considered coincident, but the doublet in between them in spike train 2 is not judged as coincident with either of them. In contrast, for A-SPIKE-synchronization the coincidence windows are adapted to the distribution of all ISIs in the dataset and the two sides of the coincidence window are allowed to be of different length. With this change each of the spikes in the doublet becomes coincident with one of the spikes (the respective closest one) in spike trains 3 and 4.

As a by-product of the adaptation, A-SPIKE-synchronization also increases the coincidence window coverage within and at the edges of a burst and thus matches as many spikes as possible. For SPIKE-synchronization many of these spikes would be ignored due to the unreasonably small coincidence windows. This phenomenon occurs very often with real data. An example containing two small and one large burst event is shown in Fig. 8. In the first two events A-SPIKE-synchronization is able to detect a few additional coincidences compared to SPIKE-synchronization. The difference is much more pronounced for the third and largest event. Here for SPIKE-synchronization many potential matches are left out and this leads to a rather low overall value of 0.238. Instead, when A-SPIKE-synchronization is used, there are almost 45% more matched spikes within the burst and this strongly increases the overall synchronization value to 0.345.

Fig. 8C clearly shows that the additional spike matching of A-SPIKE-synchronization only occurs in the high frequency events for which small differences in the ISIs cause gaps between the coincidence windows of adjacent spikes. Coincidences outside of these high frequency events are not affected.

2.5.3. Systematic evaluation of the influence of bursts

Next we test how the effect of the automated threshold changes when spikes are forming tighter bursts (Fig. 9). To do this we first create two Poisson spike trains which are divided into four equally long segments. These segments are then increasingly compressed which prolongs the ISIs between them such that the total length remains constant (Fig. 9A). We use the relative length of the interburst intervals \( R \) as a parameter and track the difference between the adaptive and the original versions. The results for the ISI-distance and the SPIKE-distance are very similar and we only show the latter. From Fig. 9B we can see that the SPIKE-distance decreases almost linearly with \( R \) since the relative importance of the common silence in the interburst intervals increases. The adaptive version decreases sub-linearly with the largest absolute difference between the two measures occurring around \( R = 0.4 \). For higher \( R \)-values the reduction of the burst length overshadows the increases in similarity at burst times and the difference increases up to a point and then starts to decrease. The relative difference increases over the whole interval (data not shown, but can be appreciated by observing the difference approaching the SPIKE-distance value toward \( R = 1 \)).

While for the SPIKE-distance the interburst intervals have an effect on the overall value, SPIKE-synchronization is sensitive to the matching of spikes only and is based on one coincidence indicator value per spike. Thus, the effect is increasing only until all possible spike pairs within the bursts are matched. For our example the increase saturates at \( R = 0.4 \) (Fig. 9C) at which point all possible spike pairings (encompassing roughly half of the spikes) have been identified. This is in agreement with what we demand from a distance sensitive to bursting structure for a systematic increase of the ratio between interbursts intervals and synchronous bursts.

2.5.4. Application to real data: reliability of neurons

In order to demonstrate the effects of the adaptive generalization in a more realistic scenario, we re-analyze data previously used to study the effect of membrane potential resting state on neuronal reliability (Zeldenrust et al. (2013), see Appendix B.2 for details on the recordings). When in the original study frozen noise was injected into thalamocortical relay cells of rats, it was found that the reliability of the cell response increases with depolarization (Zeldenrust et al., 2013).

Here we use both the original versions and the adaptive generalizations of all three measures to assess the reliability of the responses from the two neurons for which all four levels of membrane potential were recorded. The adaptive versions use a threshold obtained from the data by pooling all spike trains of each level and trial together. In Fig. 10 we show the results of the cell with the more prominent effect but we get similar results for the other cell as well. The cells analyzed were recorded three times for each
Fig. 7. Largest absolute and largest relative change between ISI-distance and A-ISI-distance (A and B) as well as SPIKE distance and A-SPIKE-distance (C and D) for the spike train set shown in Fig. 5. In both cases the two measures show a different order of similarity. The original distances increase from the first to the second pair, while the adaptive extensions decrease. The first pairs attain distance values in between the second pairs, which results in a different order of similarity between the measures (see Fig. 6). Upper subplots: the spike train pairs with the largest changes. Lower subplots: respective original distance vs. adaptive version profiles with the difference between the two profiles emphasized. The distance values for the first (second) pair are shown on top (at the bottom). They are also marked by a dashed line for the original distance and by a solid line for the adaptive distance.

holding membrane potential and reliability was assessed by trial to trial variations. For the highest hyperpolarization (Fig. 10A) the original SPIKE-distance yields spuriously high values for the local dissimilarity during the bursts, since it only evaluates the local context. Even when the A-SPIKE-distance takes the global context into account, both measures agree that there are large dissimilarities in the spike trains.

For the most depolarized state (Fig. 10B) the membrane potential is considerably closer to the action potential threshold. The patterns are closely matching the burst positions of Fig. 10A, but also additional events appear. The neuron no longer responds in clearly distinguished bursts and it is considerably more difficult to determine where a burst begins or ends. Since the generalized version adapts to time scales found in all the spike trains, it is able to distinguish when a burst-like pattern emerges and considers them as more similar.

As can be seen in Figs. 10C and 10D, the original versions, without adaptation and only using the local context, attain a higher level of similarity for $-60\,\text{mV}$ than for $-50\,\text{mV}$, which contradicts both the results in the original study and the results for SPIKE-synchronization (Fig. 10E). Since the adaptive versions are able to make use of the global context of all the spike trains, they...
3. Rate-independent extension

Sometimes in neuroscience one is interested in the pure similarity of spike timing, independent of any differences in spike rates. Thus there is the need for a measure which can identify differences in spike timing but is able to ignore any differences in rate between the spike trains. Here we propose such a rate-independent extension for the A-SPIKE-distance.\footnote{The A-ISI-distance is a measure of instantaneous rate difference and a rate-independent measure of rate difference makes little sense. A-SPIKE-synchronization is rate-dependent by definition, since it is calculated as the average value of spike-based coincidence indicators (Eqs. (20) and (23)).}

3.1. RIA-SPIKE-distance

In order to understand how rate-independence for A-SPIKE-distance is achieved, we need to separate Eq. (11) (Section 2.2) for the pairwise A-SPIKE-distance profile into its three components.

The first two components are the mean of spike time dissimilarity and the normalization to firing rate

$$S_{m,n}(t) = \frac{S_n(t) + S_m(t)}{2} \cdot \frac{1}{\max(|\tau_{ISI}(t)|, T)},$$

(26)

where $S_n(t)$ and $S_m(t)$ are the weighted spike time differences for spike trains $n$ and $m$ defined by Eq. (10). The third component is a weighting of the spike time dissimilarity according to the firing rate difference that is applied to the first component

$$\frac{S_n(t) \tau_{ISI}(t) + S_m(t) \tau_{ISI}(t)}{\tau_{ISI}(t)}.$$

(27)

The rate-independent adaptive SPIKE-distance (RIA-SPIKE-distance) simply leaves out this last weighting and can thus be written as

$$S_{m,n}^{RIA}(t) = \frac{S_n(t) + S_m(t)}{2} \cdot \frac{1}{\max(|\tau_{ISI}(t)|, T)}.$$

(28)

The RIA-SPIKE-distance shares all the properties of A-SPIKE-distance, but it only evaluates normalized spike timing differences, whereas the A-SPIKE-distance additionally uses differences in rate to determine similarity.

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attain results without this spurious dissimilarity and thus for higher membrane potentials the similarity increases monotonously.

A-SPIKE-synchronization works slightly differently (Fig. 10E). Due to the tight bursts that cause excessively small coincidence windows, the largest difference occurs for the hyperpolarized states. However, both versions agree as quantified by spike to spike matching in the response patterns clearly show a monotonous increase over the baseline membrane potential. In summary, the results obtained by the A-SPIKE-distance and A-ISI-distance seem to be appropriate and more in line with the original results.

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Fig. 8. Real data example from MEA recordings (see Appendix B.1 for more details). Ten spike trains from the dataset are plotted and their coincidence windows are drawn as obtained by SPIKE-synchronization (A) and A-SPIKE-synchronization (B). The difference is plotted in (C). Due to the adaptive coincidence windows, A-SPIKE-synchronization is able to match around 45% more spikes between bursting spike trains than SPIKE-synchronization. As in Fig. 3, the color scale is gray-black in (A) and (B) and white-black in (C).

Fig. 9. Effect of bursts on the adaptive versions evaluated by using the relative length $R$ of interburst intervals. The values are averaged over 10 realizations. (A) Five spike train pairs with increasing levels of burstiness for one example realization. (B) Effect of burstiness on the difference between A-SPIKE-distance and SPIKE-distance. The graph for the ISI-distance looks very similar and is thus omitted. (C) Equivalent results for A-SPIKE-synchronization. The $R$-values of the examples in (A) are marked in (B) and (C) as dotted vertical lines.
3.2. Results

In this section we compare the RIA-SPIKE-distance to the regular A-SPIKE-distance regarding their response to differences in rate. First, in Fig. 11A we look at Poisson spike trains with different rate ratios. The regular A-SPIKE-distance exhibits a clear rate dependency obtaining its lowest value for spike trains with identical rates and increasing for higher rate differences. The RIA-SPIKE-distance on the other hand starts near 0.25 and remains relatively constant for all rate ratios. These deviations from perfect rate-independence occur because of the irregularities of the Poisson spike trains. When we repeat the same analysis with steady rate instead of Poisson spike trains (Fig. 11B), thereby removing the effects of the Poisson statistics, the RIA-SPIKE-distance exhibits indeed perfect rate-independence.

Regarding the original distances, in Fig. 11A they would show very similar behavior to the adaptive generalizations. Only for rate ratios close to 1 there would be a small increase due to coincident burst-like events within the Poisson spike trains. In Fig. 11B the curves would overlap perfectly since there is only one time scale in steady rate spike trains (both results not shown).

4. Discussion

In this manuscript we introduce adaptive generalizations to the three existing measures ISI-distance, SPIKE-distance and SPIKE-synchronization as well as a rate-independent extension to the generalized SPIKE-distance. These new measures address two distinct problems.

The adaptive generalizations allow to disregard spike time differences that are not relevant on a more global scale. By means of a specifically constructed library of both stereotypical and real data spike trains, we can show that both A-ISI-distance and A-SPIKE-distance indeed yield improvements for pairs of spike trains containing different time scales without exhibiting any unwanted side effects in other examples. Thus the changes are both sensitive and specific. Regarding the size of the changes, even if they are seemingly small on an absolute scale, the relative changes can be very significant. For our test set the largest relative change reaches 29% for the A-ISI-distance and even up to 62% for the A-SPIKE-distance. With a more qualitative approach we then show that A-SPIKE-synchronization fixes the problem of SPIKE-synchronization which demands an unreasonably high accuracy for spike doublets and coinciding bursts. By introducing a global reference frame, it manages to match spikes more efficiently (for our test data we found an increase of 45%).

In order to test the adaptive measures methodologically we tested them in a controlled environment where two Poisson spike trains were split into bursts using increasingly large interburst intervals. We designed the adaptive extension to be sensitive to bursting structure, therefore for increasing relative length of interburst intervals we expect a larger difference between the original and the adaptive versions. We show that the relative difference indeed increases monotonously with an increase in the ratio between interbursts interval and bursts.

The absolute difference obtains its maximal value when the differences ignored in the bursts are large and the bursts are long enough in comparison to the total length of the recording. When very similar spike trains are compared their relative difference
becomes dominant and internal structures of coinciding bursts become less relevant.

Additionally, we apply the measures to a dataset previously analyzed for reliability and find that the adaptive methods agree with the previous results better than the original versions. The A-ISI-distance and the A-SPIKE-distance seem to yield more reasonable results than the ISI-distance and the SPIKE-distance. On the other hand, when the coincidence windows of the original version get spuriously small, A-SPIKE-synchronization can match spikes much more efficiently. The effect can be especially meaningful in applications in which leader-follower relationships based on the temporal order of spikes are determined (Kreuz et al., 2017).

The rate-independent extension on the other hand focuses on spike time accuracy while disregarding rate differences in the two spike trains. The original SPIKE-distance considers spike time differences but also has a feature that takes into account the firing rate difference between the spike trains. However, sometimes only the spike time accuracy is of interest and for that purpose the RIA-SPIKE-distance disregards any deviations in firing rate. We can show that the RIA-SPIKE-distance is approximately rate-independent for Poisson spike trains (apart from minor statistical effects) and perfectly rate-independent for strictly periodic spike trains. With this final addition we have completed the picture, since we now have measures that are sensitive to rate only (A-ISI-distance), to timing only (ARI-SPIKE-distance), and to both at the same time (A-SPIKE-distance).

The adaptive generalizations are implemented for cases where we have prior knowledge of the system or where we want to reduce the importance of very small details. However, one has to be careful with this method. If the threshold parameter that defines the minimum relevant time scale (MRTS) is chosen too high, this can introduce spurious synchrony. To facilitate the selection, we introduce a method for automatically extracting the threshold from the spike train data. This is done by using the second moment the ISI-distribution of the whole dataset, thereby giving more weight to longer ISIs.

Here it is important to note that while this automated estimation of MRTS gives us a threshold value for each dataset, one has to be very careful when comparing results obtained with different threshold values. Thus, one cannot use the adaptive version for two recordings from the same source without using the same threshold for both recordings, even if the ISI-distributions differ. In such cases, the preferable option would be to combine the ISI-distributions before calculating the threshold and to use the resulting value for both recordings. However, this might not work in all cases. For example, recordings before and during an epileptic seizure can have very different ISI-distributions. This means that a globally meaningful threshold cannot be extracted due to a very bi-modal distribution of all the ISIs from the whole recording. The resulting threshold would be in between the two modes which would cause the adaptive measures to basically consider one of the recordings as a long burst and the other as an almost silent period. Thus, in cases where a suitable threshold cannot be found, it is preferable to just set it to zero and consider only local information. This is equivalent to using the original versions.

Many time scale parametric measures like the Victor–Purpura and the van Rossum distance use a parameter to define the time scale of the system. The threshold set for the adaptive versions is philosophically different in the sense that it does not define a single time scale, but sets a line below which the effects of the smaller time scales are being toned down. All different time scales are still considered at the same time, but weighted differently depending on how they compare to the threshold.

Other measures that deal with multiple time scales exist. For example, Lyttle and Fellous have proposed a metric to specifically assess the similarity of spike trains with bursts or common silent periods (Lyttle and Fellous, 2011). While in the proposed adaptive measures the time scale parameter is limiting full time scale independence of the original measures, in many measures the time scale is a fixed value. With the method proposed by Lyttle and Fellous they can detect bursts as well as silent periods. However, this comes with a cost, since the method requires two time scale parameters and three additional parameters: length of minimum silent period, length of burst ISI, minimum number of spikes in a burst, scaling factor to decide how important bursts are in comparison to single spikes, and another factor to decide between importance of burst and silent period detection. While the large array of options gives the experimenter a powerful tool and provides more control over the analysis, it also increases the complexity of the overall experiment. This may cause problems, in particular when the data has many dimensions. Similarly, Rusu and Florian have introduced a new class of metrics (Rusu and Florian, 2014). The max–metric and the modulus-metric are well suited for measuring distances between spike trains where information is encoded in bursts but single spike accuracy within burst is not relevant. The max–metric depends on the kernel chosen and a time scale parameter deciding its size. The modulus-metric is parameter free like the ISI-distance, the SPIKE-distance, and the SPIKE-synchronization. This is achieved by using a very simplified kernel. However, the results obtained with both methods are not normalized. Thus based on the dissimilarity value alone it is not possible to say anything about the similarity of the two spike trains, but only about the order of different pairs.
Another often used alternative to spike train distances are correlation measures (see e.g. Cutts and Eglen, 2014). However, these measures traditionally require windowing or binning and this creates the problem that their performance can depend crucially on the window length or bin size and also on the starting points and the overlap of the windows which clearly reduces the objectivity of the results.

The results confirmed our initial expectation that the main differences between the adaptive generalizations and the original measures is in their assessment of the similarity of bursty data. Since bursts are ubiquitous and have been identified as an important area of neuroscience research (see e.g. Izhikevich et al., 2003; Sherman, 2001), there is a strong need for this kind of similarity measurement. For the ISI-distance, a method has been proposed for evaluating the similarity of bursty data by identifying bursts and assigning spikes at the beginning of the bursts (Qu et al., 2016). However, burst detection is a notoriously difficult problem for which rather complicated methods have been developed (see for example Kapucu et al., 2012). Thus, a measure based on assigning spikes to bursts inherits the problems of burst detection. Another problem with the measure proposed in Qu et al. (2016) is that it disregards differences in spiking behavior within the bursts. In contrast, our adaptive versions do not detect bursts at all, but automatically adapt their behavior whenever there are burst-like features in the data.

All the measures presented here are symmetric and thus invariant to the order of the spike trains. Recently we have developed a complementary directional approach consisting of two new measures called SPIKE-order and Spike Train Order (Kreuz et al., 2017). This approach utilizes the adaptive coincidence detection of SPIKE-synchronization to first sort multiple spike trains from leader to follower and then to quantify the consistency of the spatio-temporal propagation patterns. A natural continuation of the work presented in this article would be to use the adaptive measures for this new approach as well.

We would like to finish by pointing out that the implementations of both the original and the extended measures are provided online in three separate free code packages called SPIKY2 (Kreuz et al., 2015) [Matlab GUI], PySpike3 (Python) (Mulansky and Kreuz, 2016) and, most recently, cSPIKE4 [Matlab command line with MEX-files].

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Appendix A. Edge effect correction and treatment of special cases

Here, we deal with some subtle details in the definitions of all three measures A-ISI-distance, A-SPIKE-distance and A-SPIKE-synchronization. First, in Appendices A.1 and A.2, we correct the edge effect by providing definitions for the periods before the first and after the last spike in a spike train (for which the interspike interval is not defined). This is necessary to guarantee that all measures are well-defined for the whole recording interval. Subsequently, in Appendices A.3 and A.4, we deal with the two special cases of empty spike trains and spike trains with only one spike. Even if some spike trains are empty or very sparse, all measures should still be defined in a way which is consistent with the regular definitions.

A.1 Edge effect correction for A-ISI- and A-SPIKE-distance

Since the A-ISI- and the A-SPIKE-distance are time-resolved and are based on ISIs defined by Eq. (3), there is ambiguity at the edges before the first spike and after the last spike. To resolve this ambiguity we need to add auxiliary spikes. For the beginning of the spike train, we assign an auxiliary spike at the maximum of the distance between the start of the observation interval and the first spike, and the first known ISI

\[
\tau^{(n)}_{\text{aux}} = \tau^{(n)}_1 - \max(\tau^{(n)}_1 - \tau^{(n)}_2, 0).
\]

This definition assumes that the rate stays the same at both sides of the spike unless the edge is too far away for this to be true, in which case the auxiliary spike is assigned at the edge. Analogously, the time of the auxiliary spike at the end is

\[
\tau^{(n)}_{M\text{aux}} = \tau^{(n)}_M + \max(\tau^{(n)}_M - \tau^{(n)}_{M-1}, 0).
\]

If the first or last spike is at the edge, no edge correction is necessary at that end. This defines the ISI which is then used not only for the IS-distance but also for the A-SPIKE-distance and A-SPIKE-synchronization.

An auxiliary spike used for the edge correction is basically treated as any other spike, for example they can be the nearest neighbor to a real spike. But there is one exception: In order to avoid artificial synchrony at the edges in the A-SPIKE-distance, they use the distance to the nearest neighbor from the first/last real spike

\[
\Delta_1 = \min(\Delta^{(n)}_1), \quad \text{and} \quad \Delta_M = \min(\Delta^{(n)}_M).
\]

A.2 Edge effect correction for A-SPIKE-synchronization

For the A-SPIKE-synchronization profile we first apply the edge effect correction described above and then calculate the coincidence windows following Eqs. (14) and (15).

For cases when there is a spike right at the edge, we use the one ISI that exists for setting the coincidence window of the spike to

\[
\tau^{(n)} = \frac{1}{2}\tau^{(n)}_{S(n)} \quad \text{and} \quad \tau^{(n)} = \frac{1}{2}\tau^{(n)}_{S(M)}.
\]

We also determine that an auxiliary spike can under no circumstance be part of a coincidence nor can it have a coincidence counter. Finally, an auxiliary spike does not count as a spike in the normalization.

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2 http://www.fliscn.cn/users/thomas.kreuz/Source-Code/SPIKY.html.
3 http://mariomulansky.github.io/PySpike/.
4 http://www.fliscn.cn/users/thomas.kreuz/Source-Code/cSPIKE.html.
A.3 Special cases for A-ISI- and A-SPIKE-distance

Empty spike trains and spike trains with only one spike do not provide the ingredients needed to apply Eqs. (A.1) and (A.2).

In order to define the ISI of an empty spike train without any spikes, we assign auxiliary spikes to its edges, the beginning and the end of the recording interval. This is the only interval for which we can guarantee that there were no spikes.

However, while we can now use Eq. (3), Eq. (A.3) for the distance to the nearest neighbor of the auxiliary spikes is still ill-defined, since there are no real spikes. In this case a value is assigned exactly as in Eq. (7) and the nearest neighbor can either be a real or another auxiliary spike. A very reasonable implication of this definition is that two empty spike trains will be considered equal by both measures.

Similarly, it is not possible to assess the rate at either side of a single spike. The most reasonable auxiliary spike location is again at the edge of the recording. Thus for both cases, the auxiliary spikes are assigned at the edges as

\[ t_{\text{aux}}^{(n)} = t_e \quad \text{and} \quad t_{\text{aux}}^{-1} = t_e \]  \hspace{1cm} (A.5)

and this completes the definitions for the A-ISI- and the A-SPIKE-distance.

A.4 Special cases for A-SPIKE-synchronization

For A-SPIKE-synchronization the situation is slightly different, since it is not continuous but only defined at the times of the spikes. This means that by definition an empty spike train cannot have synchronous spikes and thus has no value. In case all spike trains are empty, we set A-SPIKE-synchronization to 0, i.e. empty spike trains are considered to be perfectly synchronous. If a spike train contains only a single spike, we use half the spike train length to define the coincidence window for the spike as

\[ t_1^{(n)} = \frac{1}{2} (t_e - t_s). \]  \hspace{1cm} (A.6)

These special cases complete the definition of A-SPIKE-synchronization.

Appendix B. Experimental recordings

B.1 Microelectrode recordings from mouse cortical cells

The electrophysiological data analyzed in Sections 2.5.1 and 2.5.2 were recorded in the group of Prof. Jari Hyttinen at Tampere University of Technology / BioMediTech, Tampere, Finland. These recordings were performed prior to and independently from the design of this study.

Between 5000 and 250,000 commercially available primary mouse cortical cells (A15586, Gibco, Thermofisher) were plated on five microelectrode arrays (MEAs; four 60MEA200/30IR and one 60HDMEA30/10IR, all purchased from Multi Channel Systems, Reutlingen, Germany) following the protocol of Hales, Rolston, and Potter (Hales et al. 2010). The dishes were coated with poly-L-lysine (Sigma–Aldrich, St. Louis, MO, USA) and laminin (L2020-1MG, Sigma–Aldrich). The medium for the MEA cultures was replaced three times a week. All MEAs with cells were kept in an incubator (+37 °C, 5% CO2, 95% air) prior to and between recordings. Data were recorded three times a week between the 4th and the 35th day in vitro. Every recording lasted five minutes and was performed with 25 kHz sampling rate. Spike detection was carried out by setting an amplitude threshold at five times the standard deviation of the signal–noise level and the spike time stamps were stored with the Neuroshare Library for MATLAB (Multi Channel Systems). We used two recordings for our examples and test sets.

The five real data spike trains used in the test set (spike trains 26–30 in Fig. 5) were selected from these data by hand to represent different time scales but chosen such that spike numbers were quite constant and comparable to the artificial examples.

B.2 Patch clamp recordings of rat thalamocortical relay cells

The electrophysiological data analyzed in Section 2.5.4 were recorded at the Swammerdam Institute for Life Sciences, University of Amsterdam, the Netherlands. Again, these recordings were performed prior to and independently from the design of this study. The experiments carried out on brain slices from Wistar rats (Harlan, Netherlands; postnatal days 12–16) were approved by the animal welfare committee of the University of Amsterdam.

For details on the animals, slice preparation and electrophysiological recordings, see Zeldenrust et al. (2013). In the current-clamp measurements the cell was injected with current that consisted of a DC component with superimposed noise: a computer generated (MATLAB) time series of Gaussian distributed random numbers of a length of 300 s, filtered by an exponential filter with a time constant \( \tau = 10 \text{ ms} \) and a standard deviation of \( \sigma = 100 \text{ pA} \). A slow feedback system controlled the background DC current to stabilize the membrane voltage at one of the specified values (–80 mV, –70 mV, –60 mV or –50 mV) before the actual recording started; after the start this DC current component was fixed. The same frozen (=an exactly reproduced computer generated) noise train was injected into the soma of the TCR neuron for every repetition of the experiment. Signals were filtered at 5–10 kHz and sampled at 10–20 kHz.

The recordings consisted of trials from five different cells of which only two included trials for all four levels of membrane potential. The cells analyzed were recorded three times and reliability was assessed by trial to trial variations.

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