Detection of Listeria innocua on roll-to-roll produced SERS substrates with gold nanoparticles

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The rapid and accurate detection of food pathogens plays a critical role in the early prevention of foodborne epidemics. Current bacteria identification practices, including colony counting, polymerase chain reaction (PCR) and immunological methods, are time consuming and labour intensive; they are not ideal for achieving the required immediate diagnosis. Different SERS substrates have been studied for the detection of foodborne microbes. The majority of the approaches are either based on costly patterning techniques on silicon or glass wafers or on methods which have not been tested in large scale fabrication. We demonstrate the feasibility of analyte specific sensing using mass-produced, polymer-based low-cost SERS substrate in analysing the chosen model microbe with biological recognition. The use of this novel roll-to-roll fabricated SERS substrate was combined with optimised gold nanoparticles to increase the detection sensitivity. Distinctive SERS spectral bands were recorded for Listeria innocua ATCC 33090 using an in-house build (785 nm) near infra red (NIR) Raman system. Results were compared to both those found in the literature and the results obtained from a commercial time-gated Raman system with a 532 nm wavelength laser excitation. The effect of the SERS enhancer metal and the excitation wavelength on the detected spectra was found to be negligible. The hypothesis that disagreements within the literature regarding bacterial spectra results from conditions present during the detection process has not been supported. The sensitivity of our SERS detection was improved through optimization of the concentration of the sample inside the hydrophobic polydimethylsiloxane (PDMS) wells. Immunomagnetic separation (IMS) beads were used to assist the accumulation of bacteria into the path of the beam of the excitation laser. With this combination we have detected Listeria with gold enhanced SERS in a label free manner from such low sample concentrations as $10^4$ CFU ml$^{-1}$.

Introduction

Foodborne diseases represent a serious public health issue. The incidence of epidemics related to food pathogens has increased significantly due to the greatly accelerated range and speed of distribution that has resulted from the increasingly global trade network for food products.1 For this reason, food safety authorities around the world have realized the need for a strict regulatory framework, including an exhaustive food testing regime.2,3 Traditional methods for the detection of bacteria, include direct culture and colony counting, polymerase chain reaction (PCR) and immunological methods. These are all extremely labour intensive and time consuming;4,4 the extent to which a rapid and efficient food testing regime can be achieved using the currently available methodologies is limited.

Raman spectroscopy is a promising new methodology for bacteria detection, with many advantages including identification of the specific species of the bacteria, rapid detection, multiple simultaneous analyses and being label free.7–11 The identification of the species of bacteria through Raman
sensitivity and requires the disintegration of the solid matrix to accelerate the bacteria growth to a detectable amount. The conventional Raman spectroscopy cannot reach this level and the signal thus needs to be amplified. This can be achieved through the use of noble metallic materials, for example gold or silver, to trigger localised surface plasmons. Surface Enhanced Raman Scattering (SERS) is a special type of Raman spectroscopy, where irregular or patterned metal substrates or metal nanocollodics of different shape and size can be used for the signal enhancement.

Typically the best enhancement effect is achieved with silver induced SERS. However, the use of silver has some drawbacks. As a substance it is antimicrobial and thus affects the sample under inspection. It is chemically quite reactive and the stability and reproducibility of the silver substrates and colloids (AgNP) can also be an issue. Gold is preferred in microbe detection as it is stable, non-toxic and has the optimal excitation wavelength in the near-infra red region, reducing auto-fluorescence issues generated by the microbes.

Among the foodborne pathogens Listeria monocytogenes is the most common culprit in causing death due to food poisoning. The fatality rate for L. monocytogenes infection is relatively high, ranging from 20 to 30%. L. monocytogenes is an especially difficult pathogen to control, as a result of its tolerance to a wide range of temperatures and pH conditions. The detection of Listeria spp. with SERS has been studied previously with different SERS enhancers including different SERS substrate approaches and SERS colloid research. The SERS substrates have several advantages over the colloids; these include more consistent patterns without unforeseen aggregation and the ability to act as a base for the entire analysis chip. On the other hand, colloids can reach better sensitivity and be preferable when there is a need to detect features in the region of a larger organism like bacteria.

The direct detection of bacteria in food is difficult due to background signals and requires the disintegration of the solid food containing the bacteria, e.g. by mechanical methods, followed by culturing of the bacteria at elevated temperatures in the food matrix to accelerate the bacteria growth to a detectable level. Weidemaier et al. has studied the detection of L. monocytogenes inside the food matrix with the help of immuno-magnetic beads and nanoparticle SERS tags with antibodies, as they point out, the method is sensitive to the extent to which the magnetic particles can be concentrated within the area of the laser beam and care must be taken to succeed with reproducible pelleting of the magnetic particles. A more common method for bacteria detection is to remove the bacteria from the food matrix, often with immunocapture and subsequently pre-enrich the concentration before detection. Although the pre-enrichment technique requires culturing this can be used as a normalising factor for the state of the pathogen. The growth of Listeria at different temperatures, for example 4, 25 or 37 °C, produces bacteria with different amount of flagella and a different level of virulence. This affects the spectral fingerprint of the bacteria; in order to obtain reproducible spectra for bacteria, the same growing conditions in addition to detection processes are required.

In previous research, it has been shown that it is possible to differentiate bacteria through SERS analysis. Preliminary results also indicate that SERS can be used for identifying bacteria and spores even at a strain level. Usually this requires a high concentration of bacteria. With low concentration the assistance of immunocapture may be needed for the separation of different bacteria. The genus Listeria consists of fifteen species from which only Listeria monocytogenes is pathogenic to humans. Immunocapture by current commercially available antibodies can seldom distinguish between the Listeria species. There are studies focussing on the production of high quality antibodies only for L. monocytogenes. The presence of non-pathogenic Listeria such as Listeria innocua may, however, indicate also contamination with L. monocytogenes. Furthermore, as the morphologic structure of L. innocua is similar to L. monocytogenes and their Raman/SERS-spectra are quite similar, L. innocua can be used as a model for Listeria detection.

The detection of Listeria with SERS has been previously studied by several research groups. The majority of studies have focussed on the detection of Listeria at high concentration, 10⁸ to 10¹⁰ CFU ml⁻¹ and many have used chemometric analysis for the separation of Listeria spectra from the spectra of other pathogenic bacteria. Fewer studies have focussed on lowering the detection limit of the SERS procedure for Listeria detection than on the acquisition of representative spectra. Chen et al. have developed a method for detection of L. monocytogenes and L. innocua by in situ synthesis of silver nanoparticles. The limit of detection for the model sample L. innocua was found to be 10³ CFU ml⁻¹. The assay for bacteria detection was, however, performed for bacteria in pure water and required an extra incubation step with the silver colloids and two washing steps after the incubation.

The objective of this study was to develop a simplified and affordable method for label-free detection of Listeria with high sensitivity that is possible to perform on a structured SERS substrate. The conventional way for fabricating structured SERS substrates is to use methods such as spin-coating, dip coating, chemical vapour deposition, electrochemical synthesis, electron beam lithography and etching. However, they are not optimised for manufacturing single use chips in terms of through-put volume or cost. There are also many methods such as liquid–liquid interface formation, pulsed laser deposition on microscope slides and reduction of gold chloride in natural rubber membranes which have been only tested in lab scale as batch fabrication. The fabricated sensor areas are often small and the fabrication methods are difficult to transfer into high volume production required of truly disposable sensor
chips. Our approach is to fabricate the structured SERS substrates on polymer webs in large scale with UV imprint lithography. This enables the fabrication of large sensor surface areas which can be easily cut into smaller SERS substrates.\textsuperscript{40,41} The fabricated SERS substrates are coated with a thin layer of gold by evaporation before integration of hydrophobic sample wells. This SERS platform is suitable for low cost high volume production and is practical for one-time use, which diminishes the contamination issues often encountered in microbe detection. Gold colloids were added to gain additional plasmonic enhancement. The method uses immunomagnetic separation (IMS) beads as bacteria cell concentrators and the only washing steps occur during the pre-enrichment phase. SERS enhancement of different types of gold nanoparticles with \textit{Listeria} was studied and the colloids with the best enhancement effect were used in combination of R2R nanostructured gold SERS substrates.

**Experimental**

**Gold nanoparticle synthesis**

Ultrapure nanoparticle fabrication. Hurricane Spectra Physics Ti/sapphire laser operated at 800 nm with pulse duration 110 fs and repetition rate 1000 Hz was used for formation of gold nanoparticles (AuNPs) with a two-step approach.\textsuperscript{42,43} In the first step, a gold target was immersed in 5 ml of deionized water at 10 mm below the water surface. Colloidal solution of AuNPs was produced by ablating the target at 150 \( \mu \)J per pulse for 30 minutes. The target was moved during the ablation step when material was collected from larger area. In the second step, additional laser fragmentation was performed to narrow the size distribution of AuNPs and to improve their stability. The fragmentation was performed by focussing a laser beam with 85 \( \mu \)J per pulse fluorescence in the centre of the liquid volume that was stirred with a permanent magnet for 60 minutes.\textsuperscript{44}

AuNP fabrication for medium and large size particles. Colloidal AuNPs were synthesized by following the Frens-method.\textsuperscript{44} 100 ml of 0.01% (wt/vol) HAuCl\(_4\) aqueous solution was heated to boil under vigorous and continuous stirring, followed by dropwise addition of 0.6 ml of 1% (wt/vol) trisodium citrate solution. The solution was kept boiling for approximately 1 h until the color changed to light red. The final AuNP-solution was prepared by centrifugation at 3500 rpm for 5 minutes (Eppendorf model 5430R) and subsequently followed by the removal of the supernatant. The final dark red AuNP-solution with a concentration of about 5500 mg l\(^{-1}\) was used and partially diluted in ratio 1 : 5 in H\(_2\)O.

AgNPs with the average size of 40 nm were purchased from Sigma-Aldrich for reference measurements with the commercial time-gated Raman spectrometer.\textsuperscript{45}

**SERS substrate fabrication**

The SERS patterns were imprinted on top of a poly(methyl methacrylate) (PMMA) polymer sheet with roll-to-roll UV-nanoimprint lithography.\textsuperscript{44} The produced polymer webs and die-cut sheets before and after gold deposition are presented in Fig. 1. Reverse gravure technique was used to apply UV-curable lacquer on top of the PMMA web. Embossing reel was used to imprint the SERS patterns and the lacquer was cured through the PMMA web with UV light exposure. After die-cutting SERS substrates from the roll, a 240 nm gold layer was added by evaporating on top of the polymer SERS surface.\textsuperscript{44}

**PDMS well integration**

Sample wells were created into 1 mm thick PDMS sheets (Wacker, Elastosil) by biopsy punches of a diameter of 1–2 mm. These PDMS wells were bonded onto the polymer SERS substrates by physical adsorption. The hydrophobicity of the wells forces the sample to retreat inside the PDMS well and have contact with the gold layered patterned SERS surface.

**Cultivation of \textit{L. innocua} and IMS bead separation**

\textit{L. innocua} ATCC 33090 was cultivated in LEE Broth (Labema, Lab M Limited, pH 7.2 ± 0.2) at 35 °C for 20 h without shaking. The concentration was analysed spectrophotometrically (Dynamica HALO DB-20S) and diluted into concentration series (10\(^3\) CFU ml\(^{-1}\) to 10\(^9\) CFU ml\(^{-1}\)) in LEE broth. IMS was performed using Dynabeads\textsuperscript{®} anti-\textit{Listeria} (Life Technologies (Invitrogen) 71006), and a Dynal Magnetic Particle Concentrator DynaMag\textsuperscript{TM} -2 (Invitrogen Dynal) as follows: 1 ml volumes of bacterial culture was added to each of the microcentrifuge tubes containing a 20 \( \mu \)l volume of Dynabeads\textsuperscript{®} anti-\textit{Listeria} (Dyna) followed by incubation at room temperature for 10 min with continuous mixing by Mix-Mate (Eppendorf). The beads were concentrated by magnetic field (in the Dynal MPC-M) onto the side of the tube for 3 min, supernatants were carefully aspirated and the samples were washed with the washing buffer (0.15 M NaCl, 0.01 M sodium phosphate buffer, pH 7.4 with 0.05% Tween 20). After that the beads were concentrated and the supernatant removed. Finally, the bead–bacteria complexes were resuspended into 100 ml of washing buffer for the SERS detection. For reference a concentration analysis was performed with 50 \( \mu \)l volumes of bead–bacteria complexes streaked onto differential selective agar \textit{Listeria} acc. to Ottaviani and Agosti (ALOA) chromogenic agar (Labema) and incubated at 35 ± 0.5 °C for 24–48 h.
SERS spectral acquisition of *Listeria innocua* and post-processing of data

Surface-enhanced Raman spectroscopy (SERS) spectra of *L. innocua* with AuNPs was detected from samples pipetted into PDMS wells integrated on top of SERS-active substrates. Sample amounts varied from 5 to 10 µl and well diameter varied from 1 to 2 mm. Bacteria samples were pipetted into the wells and the chosen AuNPs were pipetted sequentially. SERS spectra were recorded with an in-house built Raman system coupled into an Olympus microscope with a 785 nm continuous wave (cw) laser. The minimum laser power irradiation used was 10 mW with 40× magnification to excite the samples. A maximum of 40 mW was used in combination with low magnification (20×). The signal collection time was 5 seconds without averaging.

Reference spectra for *L. innocua* were recorded with 40 nm sized AgNPs by a commercial 532 nm picosecond pulsed laser time-gated Raman spectrometer (TimeGate Instruments Oy, Finland) with an average power of 10 mW, as well coupled into Olympus microscope. The signal integration time was set to cover the SERS-signal and the fluorescence decay-time from 0.9–1.6 ns. The bacteria sample was pipetted on top of a glass slide prior to the detection. TimeGate measurements where analysed with TimeGate spectral processing tool and the acquired data was baseline corrected with a simple linear algorithm in Matlab (release 2015a, Mathworks Inc., USA) after opening the data with the PLS toolbox, version 2.0 (Eigenvector Research Inc., Manson, WA, USA). Further data handling and figure plotting was executed with Origin Pro (version 9.4, OriginLab corp., USA).

Results and discussion

Methods for the detection of *Listeria innocua*

Typically *Listeria* spp. has been identified by the SERS method from highly concentrated samples, mostly in the range of 10⁷ CFU ml⁻¹ to 10¹⁰ CFU ml⁻¹. When the detected concentrations are more realistic and the bacterial cells available for the detection are fewer, then the intensity of the detected Raman peaks diminishes and many of the peaks disappear from the spectrum. Thus it is more difficult to identify the bacteria from other bacterial species and the background with incomplete spectra. In these cases the identification of the bacteria can be handled by pathogen-capture proteins while SERS is used for the detection. \(^{29}\) Grow et al. have detected *Listeria* on planar SERS substrates by capturing and accumulating bacterial cells near the surface with an antibody layer. \(^{18}\) Although they concluded that the use of antibodies was possible and identification of bacteria was successful, the use of antibodies on the surface weakened the signal. This was assumed to be due to the increased separation distance between the surface and the bacterial cells. \(^{46}\) Thus, this approach with planar SERS substrates was not optimal. Another possibility for capturing bacteria is the use of immunomagnetic separation beads which have been used in several *Escherichia coli* studies\(^ {24,35}\) and at least in one *Listeria* growth study. \(^ {24}\) Usually, the IMS beads are either removed before detection or used as a part of a customised sandwich assay with SERS labels. In order to simplify the detection process we have developed a method to detect *L. innocua* in a label-free manner with IMS beads present during the SERS detection. The bacterial cells were captured by using a commercially available IMS separation kit. The sample was placed into the hydrophobic PDMS well on top of the polymer SERS substrate as is shown in Fig. 2 with the gold nanoparticles. Without IMS beads and PDMS well the bacterial cells in the liquid droplets spread wide apart and typically due to evaporation accumulated randomly to the droplet edges. We found that by using immunomagnetic separation beads during the detection we obtained a more stable SERS signal due to the more constant settling of the heavy IMS beads on to the sensor surface. A close-up transmission electron microscopy (TEM) picture of the IMS beads and a scanning electron microscopy (SEM) picture of IMS beads on top of the patterned SERS substrate can be seen in Fig. 3a and b respectively. In order to further enhance the SERS signal and to detect the features of the bacterial cells, gold nanoparticles were added around the bacteria bound to IMS beads.

**AuNP characterisation**

In search for the optimal gold nanoparticles (AuNPs) for bacteria detection with SERS, 3 candidates were selected.
Ultrapure small AuNPs fabricated by femtosecond laser fragmentation were chosen as they could show better biocompatibility with bacteria cells than the synthesized AuNPs. The physically fabricated AuNPs lack the traces of non-reacted starting reagents, by-products, ions and surfactants, and have an additional advantage of lower background signal. Chemically synthesized medium size AuNPs and larger AuNPs were chosen to compare the signal intensity using differently shaped and sized particles. The NP size has been previously shown to matter in micro-organism detection and a rod like shape has seemed beneficial for SERS enhancement. The size and morphology of the fabricated AuNPs were retrieved by transmission electron microscopy (TEM) by using a LEO 912 OMEGA (Zeiss, Germany). One droplet of the 10 μl of aqueous nanostructure suspension was deposited onto a carbon-coated copper grid for TEM characterization. Fig. 4 shows the TEM images, the corresponding size distribution histograms calculated from TEM images of the AuNPs with Gaussian fit: small, medium and large size AuNPs respectively. Each histogram has been calculated from 100 particle sizes with ImageJ software. (g) UV-Vis spectrum for the small, medium and large size AuNPs.

The SERS effectiveness of the different sized AuNPs was studied by pipetting 5 μl of bacteria sample and 2 μl of concentrated NP solution into 2 PDMS wells positioned on top of the patterned SERS substrate. The acquired SERS spectra are presented in Fig. 5a. According to the bar plot of the intensity of 737 cm$^{-1}$ peak presented in Fig. 5b, the medium size and the large size particles gave similar intensities for a bacteria concentration of $5 \times 10^5$ CFU ml$^{-1}$. However, the large nanoparticles were chosen for further studies because the maximum of their UV-Vis spectra was closest to 785 nm and they provided more consistent spectra compared to the other AuNPs, which originated from the lower amount of background peaks thus giving a better resolution. These results strengthen the hypothesis that larger nanoparticles enhances the signal more than small round ones for microbe detection. The way the AuNPs were fabricated played a minor role in enhancing the signal. Physical ablation could not benefit the detection in such a manner which would have counterweighted the advantage of the size and the shape of the particles.

The development of the detection process

Commercial Dynabeads were used to capture the L. innocua cells for the SERS detection. The SERS signal recorded with IMS beads, possibly due to accumulation of more bacterial cells inside the excitation laser spot, was found to be 20 times stronger than the signal recorded without the beads. Fig. 6a
The captured L. innocua was first detected inside a PDMS well in a liquid state with a 40 mW laser power and a 20 x magnification. Fig. 8a shows the mean spectra for the L. innocua specific Raman bands. It can be noted that when the bacterial amount diminishes some lines stay constant showing the lines created by the traces of culture medium and buffer liquids. Thus, it can be concluded that 9 Raman bands initiating from the bacterial cells were detected. Fig. 8b shows the Raman bands created by the sample matrix and by the original cultivation media of the bacterial cells, i.e. the LEE broth. Most of the background bands seem to originate from traces of the LEE broth.

The nine Raman lines detected for L. innocua are listed in Table 1 with tentative assignments found in literature references. The dominant peak at 737 cm\(^{-1}\) has been previously suggested to originate from a glycosidic ring, adenine or CH\(_2\) rocking. Since the presence of adenine on the surface of the bacterial cell is unlikely and since the outer wall structure of Gram-positive bacteria such as Listeria spp. consists of a thick peptidoglycan structure rich in N-acetyl-glucosamine (NAG), the origin of the peak is more likely caused by a glycosidic ring mode of NAG than adenine.

The three closely aligned lines in the range of 1300–1400 cm\(^{-1}\) are interesting since three of them together have not been detected with L. innocua or L. monocytogenes in previous studies. The line 1339 cm\(^{-1}\) has been previously detected with Listeria by Luo et al.\(^{52}\) as a shifted line 1331 cm\(^{-1}\) which was suggested to originate from CH\(_2\) deformation. However, there are closer assignments to the detected 1339 cm\(^{-1}\) listed in E. coli studies. Vohnik et al.\(^{53}\) have suggested that the exact line 1339 cm\(^{-1}\) could be originating from amide III and Harz et al. suggest that the line is due to the signature of adenosine monophosphate and guanosine monophosphate, aromatic amino acids tyrosine and tryptophan. Harz et al.\(^{7}\) also have a listing very near to the second line 1374 cm\(^{-1}\) assigned to DNA. The last line of the group 1397 cm\(^{-1}\) is most likely due to the symmetric deformation of CH\(_3\) group which has also been detected for the case of E. coli.\(^{54,55}\)

When comparing the Raman bands detected for L. innocua with the previous research, it is interesting to note that the SERS spectrum in different studies varies. Liu et al. among others has stated that this could be due to the differences in the measurement conditions such as the culture broth and temperature that have been used, excitation wavelength of the
Clear when comparing the results, there is no connection between the variations in spectra and the enhancer used (silver/gold). Additionally the excitation wavelength does not seem to affect the detected spectrum.

The detection process was developed further by manually lowering the minimum laser power of the Raman system to 10 mW. This enabled the use of larger magnification with the microscope without burning of the dried specimen during the measurement procedure. The sample density on the SERS substrate was also reduced to prevent the blocking of signal by the media traces of the sample liquids. It was noted that the laser or the SERS enhancer.19,51 To test this hypothesis we recorded the SERS spectra of the same L. innocua sample with changed SERS conditions. Fig. 9 shows the peaks detected around the dominant peak 737 cm⁻¹ for 3 different SERS conditions. In the first case the combination of AuNPs on top of the patterned SERS substrate with 785 nm cw excitation was used, while in the second case a SERS spectrum was detected from the same sample on top of a glass slide with AgNPs and pulsed laser excitation at a different wavelength of 532 nm. The results are consistent. They are also similar to the third case published by Luo et al. who used AgNPs with 785 nm cw excitation wavelength. Another research group of Kairyte et al.22 used silver NPs with 1064 nm excitation with a similar outcome.

| Detected lines | Raman shift (cm⁻¹) | Tentative assignments | Reference |
|----------------|---------------------|-----------------------|-----------|
| 631            | 627/620             | Phenylalanine (skeletal) | Luo, Lin 2008,23 Maquelin et al. 2002 (ref. 56) |
| 737            | 732                 | Glycosidic ring mode of β-glucosamine (NAG), adenine or CH₂ rocking | Luo, Lin 2008,23 Cui et al. 2015 (ref. 57) |
| 968            | 955                 | N–C stretching        | Vohnik et al. 1998 (ref. 53) |
| 1142           | 1134/1130           | C–N and C–C stretch (carbohydrates) | Fan, Hu 2011,24 Chen et al. 2015 (ref. 58) |
| 1271           | 1230–1295           | Amide III             | Liu, Chen 2007,59 Lu, Al-Qadiri 2011,60 Maquelin et al. 2002 (ref. 56) |
| 1339           | 1334/1339/1338      | Deformation CH/amide III/signature of adenosine monophosphate and guanosine monophosphate, aromatic amino acids tyrosine and tryptophan | Maquelin et al. 2000,61 Vohnik et al. 1998,62 Harz, Rösch, Popp 2008 (ref. 62) |
| 1374           | 1371                | DNA                   | Harz, Rösch, Popp 2008 (ref. 62) |
| 1397           | 1392/1398           | Symmetric deformation of CH₃ groups | Fan, Hu 2011,24 Al-Qadiri, Lin 2008 (ref. 55) |
| 1450           | 1453                | CH₂ deformation (lipids) | Fan, Hu 2011,24 Cui et al. 2015 (ref. 57) |

Fig. 9 Three SERS spectra of L. innocua were compared to confirm that the measured spectrum originates from the assumed bacteria. The literature reference has been borrowed from a publication by Luo, B. Steven et al. (2008) with a concentration of 10⁶ CFU ml⁻¹ L. innocua measured with cw 785 nm laser excitation with AgNPs. The 785 nm cw laser excitation with the in-house built device has been recorded from 10⁶ CFU ml⁻¹ IMS bound L. innocua ATCC 33090 with large AuNPs inside a PDMS well on top of a patterned SERS surface with IMS beads, detected with 40× magnification. The 532 nm pulsed laser excitation is a AgNP-enhanced SERS spectra of 10⁶ CFU ml⁻¹ IMS bound L. innocua ATCC 33090 placed on top of a glass slide and 40× magnification.

Fig. 10 (a) A normalised concentration series for LOD estimation. (b) An exponential fit for the normalised concentration series in logarithmic scale for the entire series and a linear fit for the small concentrations. (c) Comparison of the 737 cm⁻¹ peak intensity for different concentration series with 5–10 μl dried IMS bound L. innocua ATCC 33090 samples placed with AuNPs into a 1–1.5 mm PDMS well on top of SERS substrate. (d) Comparison of baseline corrected Raman intensities for three of the concentration series. All figures are a mean of 9 measurement points with mean absolute deviations.
media was disturbing the SERS signal if an excessive amount of traces had dried on top of the SERS substrate. Limit of detection and repeatability of the detection process could have been enhanced further with extra washing steps for the IMS beads, but this was avoided in order to not complicate the sample handling. Fig. 10 shows the mean intensity changes of the dominant peak of 737 cm\(^{-1}\) as a function of \(L.\) innocua concentration with 40\(\times\) magnification and 10 mW laser excitation power for several concentration series. For the concentration series in Fig. 10a and b the Raman intensity was normalized by the background peak at 787 cm\(^{-1}\). The intensity of the dominant 737 cm\(^{-1}\) peak is displayed in Fig. 10b as a function of logarithmic \(L.\) innocua concentration that follows an exponential curve. For the concentration range below \(10^5\) CFU ml\(^{-1}\) the relation was found linear. Since the blank 0 CFU ml\(^{-1}\) sample exhibits a signal at 737 cm\(^{-1}\), the lowest limit of detection was considered through the deviation of the background signal generated by the sample matrix. According to the international union of pure and applied chemistry, IUPAC, the limit of detection (LOD) can be defined as the smallest concentration detected with reasonable certainty, and derived from

\[
\text{LOD} = k_{\text{sn}} S
\]

where \(s_{\text{ni}}\) is the standard deviation of the blank measures, \(k = 3\) is a numerical factor of confidence level approved by IUPAC and \(S\) is the slope of the calibration curve. \(S\) is defined as

\[
S = \Delta c / \Delta I^{1/3}
\]

where \(\Delta c\) is the change in concentration and \(\Delta I\) is the change in Raman intensity. By using eqn (1) and determining \(S\) from the linear fit shown in Fig. 10b, the LOD was calculated to be \(1.4 \times 10^3\) CFU ml\(^{-1}\). The concentration series shown in Fig. 10c and d confirm the LOD, since the deviation of the concentrations below \(10^4\) CFU ml\(^{-1}\) coincide with the deviations of the mean blank samples. This means that samples with lower concentrations cannot reliably be detected. In case of model \(L.\) innocua sample, the estimated detection time including pre-culture\(^{34}\) (6 hours) for \(10^4\) CFU ml\(^{-1}\) sample concentration, IMS preparation (15 minutes), sample deposition on SERS chip (15 minutes), SERS detection (10 minutes) and data handling (5 minutes), the total microbe analysis is estimated to be 7 hours. The time-saving of the developed method compared to the conventional official ISO 11290-1:1996/amd.1:2004 method in case of the model sample is approximately 41 hours with precultivation.

As a summary, we demonstrated in this study the use of disposable polymer SERS platforms and AuNPs with integrated sample wells for fast and simple detection of \(L.\) innocua. We have shown how the capture and deposit of the IMS bound bacteria cells onto the SERS substrate benefits the detection. In the future, the detection process could be further developed by utilizing the magnetic nature of the IMS beads on the SERS substrate for the removal of matrix traces \(e.g\). by removing the matrix with wicking.

Conclusions

This study analyses the use of different types of AuNPs in addition to a structured polymer SERS substrate for \(L.\) innocua detection. The polymer based SERS substrate has been produced with roll-to-roll fabrication and thus it is suitable for one time use due to the high volume production and the low cost per substrate. The results of this study provide new insights into \(L.\) innocua diagnostics. We also demonstrate the benefit of using immunomagnetic separation beads as an accumulation assistant of the bacteria for enhanced signal intensity. The use of novel hydrophobic PDMS wells for sample preparation on SERS chips enables controlled sample appliance and reduces mean absolute deviation of SERS signals. The limit of detection in this methodology was determined to be in the range of \(~10^4\) CFU ml\(^{-1}\) shown for the first time with label-free gold enhanced SERS using optimized AuNPs combined with an Au based SERS substrate.

Acknowledgements

This project was funded by TEKES (the Finnish Funding Agency for Technology and Innovation) through project and University of Oulu Graduate School through Infotech Oulu Doctoral Program and by Academy of Finland through FOULSENS (Grant No. 292253), M-SPEC (Grant No. 284907) and multi Diagnostics (Grant No. 290596). The financial support of the aforementioned institutes is gratefully acknowledged. We also thank Tiina Väyrynen (National Resources Institute Finland (LUKE)) for helping with the bacterial sample preparation. Yury Rjabchikov acknowledges a support from COST project (ECOST-STSM-BM1205-120416-072252) for performing experiments.

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