Surface Engineering of *Escherichia coli*–Derived OMVs as Promising Nano-Carriers to Target EGFR-Overexpressing Breast Cancer Cells

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Bacterial outer membrane vesicles (OMVs) have recently drawn a great deal of attention due to their therapeutic efficiency and ability to target specific cells. In the present study, we sought to probe engineered OMVs as novel and promising carriers to target breast cancer cells. Following the fusion of the affiEGFR-GALA structure to the C-terminal of ClyA as an anchor protein, the ClyA-affiEGFR-GALA construct was successfully expressed on the surface of ΔmsbB/ΔpagP E. coli W3110-derived OMVs. Morphological features of the engineered and wild-type OMVs were identical. The engineered OMVs induced no endotoxicity, cytotoxicity, or immunogenicity, indicating the safety of their application. These OMVs could specifically bind to EGF receptors of MDA-MB-468 cells expressing high levels of EGFR and not to those with low levels of EGFR (HEK293T cells). Interestingly, despite a lower binding affinity of the engineered OMVs relative to the positive control Cetuximab, it was strong enough to identify these cells. Moreover, confocal microscopy revealed no uptake of the modified OMVs by the EGFR-overexpressing cells in the presence of EGFR competitors. These results suggest that OMVs might internalize into the cells with EGF receptors, as no OMVs entered the cells with any EGFR expression or those pretreated with EGF or Cetuximab. Regarding the EGFR-binding affinity of the engineered OMVs and their cellular uptake, they are presented here as a potential carrier for cell-specific drug delivery to treat a wide variety of cancer cells. Interestingly, the engineered OMVs are capable of reaching the cytoplasm while escaping the endosome due to the incorporation of a fusogenic GALA peptide in the construct.

Keywords: outer membrane vesicles, epidermal growth factor receptor, breast cancer, engineering, affibody

**Abbreviations:** BSA, Bovine albumin serum; ClyA, Cytolysin-A; DLS, Dynamic Light Scattering; DMED, Dulbecco’s Modiﬁed Eagle’s Medium; E. coli, Escherichia coli; EGF, Epidermal growth factor; EGFRs, Epidermal growth factor receptors; ELISA, Enzyme-linked immunosorbent assay; ERS, Fetal bovine serum; HRP, Horseradish peroxidase; IPTG, Isopropyl β-d-1-thiogalactopyranoside; LAL, Limulus amoebocyte lysate; LB, Luria–Bertani LB; LPS, Lipopolysaccharide; OMVs, Outer membrane vesicles; mOMVs, Modiﬁed OMVs, PBS: Phosphate-buffered saline; PDI, Polydispersity index; PFA, Paraformaldehyde; PMA, Phorbol myristate acetate; RPMI, Roswell Park Memorial Institute; SDS-PAGE, Sodium dodecyl sulfate-polyacrylamide gel; TEM, Transmission electron microscopy; TLR, Toll-like receptors; TNBC, Triple-negative breast cancer.
INTRODUCTION

Outer membrane vesicles (OMVs) are a kind of proteoliposomes that exist by nature with a diameter of 20–250 nm and are shed by Gram-negative bacteria through budding of the outer membrane (Bitto and Kaparakis-Liaskos, 2017). The OMVs mainly consist of the bacterial outer membrane molecules and enclose some periplasmic components (Nokleby et al., 2007; Ellis et al., 2010; Huang et al., 2016; Pathirana and Kaparakis-Liaskos, 2016; Vanaja et al., 2016). OMVs have been established as nanoparticle carriers that can be uptaken by the cells via ligand-dependent surface receptors (Furuta et al., 2009; Parker et al., 2010; Olofsson et al., 2014). Furthermore, the capability of engineering OMVs for targeted delivery of chemotherapeutic agents to certain cancer cell types makes them an appealing option for cancer treatment (Chen et al., 2010). It is worth noting that effective cancer chemotherapy usually requires a high-dose administration of drugs as these chemo drugs are prone to rapid clearance and poor circulating half-life (Iyer et al., 2013). This can result in severe and long-lasting side effects (Miller et al., 2016). In this sense, OMVs, as the naturally occurring nanoparticle delivery scaffolds, could be expected to serve as a promising drug delivery vehicle in cancer therapy.

A wide range of epithelial tumors, including breast cancer, is known to overexpress a transmembrane protein belonging to the ErbB receptor kinase family, namely EGFR (epidermal growth factor receptor 1) (Bhargava et al., 2005; Martinelli et al., 2009; Seshacharyulu et al., 2012; Changavi et al., 2015). In this regard, triple-negative breast cancer (TNBC), the most clinically aggressive subtype of breast cancer, is also associated with EGFR overexpression. The level of EGFR expression or gene mutation status seems to be important in clinical therapy, and it is being used to select patients for a specific treatment (Masuda et al., 2012). In this context, innovative anti-EGFR therapies have been developed in the last few years, including both monoclonal antibodies and small-molecule tyrosine kinase inhibitors (Flynn et al., 2009).

Taken together, engineered OMVs targeting EGFR in triple-negative breast cancer cells may provide a potential lead to specific antitumor therapy with low toxicity. To construct AffiEGFR-OMVs, the need for caution in selecting an appropriate anchor protein is vital to ensure the effective incorporation of a target recombinant protein structure onto the surface of membrane vesicles (MV) without disrupting the vesicles or even the growth of the parent bacterium. Among the anchor proteins in E. coli, ClyA is a 34 KDa pore-forming cytotoxin with the ability to direct the desired protein to the surface of bacteria. This can be achieved by fusing the target sequence to the C-terminus of ClyA (Kim et al., 2008; Chen et al., 2010; Gujratı et al., 2014; Alves et al., 2015; Huang et al., 2016). Since ClyA is secreted on the surface of MVs of E. coli, it can thus provide an ideal platform to anchor recombinant proteins to the outer membrane (Kim et al., 2008). However, the detoxification of these OMV nanoparticles would be of great value due to enrichment of the outer membrane by LPS (Gu and Tsai, 1991). To solve this problem, LPS toxicity is partly attenuated by producing the LPS-modified OMVs harboring the strictly penta-acylated LPS from ΔmsbB/ΔpagP mutant of non-pathogenic E. coli W3110 by genetic modification (Lee et al., 2011).

In the present work, we employed bioengineered OMVs displaying an anti-EGFR affibody on their surface toward triple-negative breast cancer cells and sought to explore whether the engineered OMVs can represent a novel, safe, and targeted biological nanoparticle against triple-negative breast cancer as one of the most challenging types of breast cancer in terms of chemotherapy strategy. To expand the potential of our modified OMVs, we also utilized a fusogenic and pH-responsive amphipathic peptide, GALA peptide (Kakudo et al., 2004; Nishimura et al., 2014), thereby enabling the OMVs to escape the endosome. Functional assays were performed to assess the target specificity of the engineered OMVs toward the EGFR-positive and EGFR-negative cells. Furthermore, safety of the engineered OMVs was examined to validate their application as a novel cancer-targeting nanocarrier.

MATERIALS AND METHODS

Bacterial Strains, Cell Lines, and Reagents

The E. coli strains used in this study included Top 10F’ as a host for plasmid propagations and cloning procedures, ΔmsbB/ΔpagP W3110, and BL21 (DE3), which were used to produce the engineered OMVs and recombinant protein, respectively. The mutant host strain was kindly provided by Prof. Sang Hyun Kim (KRIIB, Republic of Korea) and the remaining two along with the protein expression vectors pET-32a (+) and pET-28a (+) were purchased from Invitrogen (Carlsbad, CA, United States). E. coli strains were grown in Luria–Bertani (LB) medium [1% (w/v) tryptone, 0.5% (w/v) yeast extract, and 1% (w/v) NaCl, pH 7.0]. The growth medium was supplemented with ampicillin (100 µg/ml) and kanamycin (50 µg/ml) when required. Restriction endonucleases and T4 DNA ligase were supplied by Fermentas (Waltham, United States) and Roche companies (Penzberg, Germany).

MDA-MB-468 (human breast carcinoma), HEK293T (human embryonic kidney), and THP-1 (human monocytic) cell lines were obtained from the cell bank of Pasteur Institute of Iran (NCBI). Cells were cultured in Dulbecco’s Modified Eagle’s Medium (DMEM) or RPMI1640 medium containing 10% fetal bovine serum (FBS), 100 U/mL penicillin, and 100 µg/mL streptomycin (GibcoBRL, Rockville, IN, United States) at 37°C with 5% CO2 in a humidified atmosphere inside a CO2 incubator. All reagents used were of analytical grade and obtained from Merck (Darmstadt, Germany) and Sigma-Aldrich (MO, United States). EGF antigen was a kind gift from Dr. Majid Golkar (Pasteur Institute of Iran, Tehran, Iran).

Preparation of ClyA-Affibody-GALA Expression Cassette

A codon-optimized 1,356 bp DNA fragment encoding His tag (Gly4Ser)3, myc tag, ZEGFR1907 affibody (Gly4Ser)3, and GALA fused to the C-terminus of Cytolysin-A gene was synthesized by
GeneRay Biotech (Shanghai, China) and delivered in an intermediate pMD18-T plasmid. To facilitate the expression procedure in E. coli W3110, we first generated a modified version of pET32a (mpET32a) in which the T7 promoter was replaced by Tac promoter. This step was performed to bypass the T7 RNA polymerase-dependent expression of our construct in E. coli W3110. Next, the ClyA-affibody-GALA construct was cloned in the HindIII/SacI site of mpET32a. Finally, the recombinant plasmid, mpET32a/ClyA-affibody-GALA, was transformed into the ΔmsbB/ΔpagP W3110 E. coli strain and the transformed strain was maintained on the solid medium supplemented with ampicillin (100 μg/ml).

Preparation of the AffiEGFR-OMVs

OMVs were isolated according to the procedure described previously by Chen et al. (2010) with some modifications. Briefly, the overnight saturated cultures of E. coli were inoculated into 1 L of LB medium supplemented with ampicillin (1:100 v/v). Subculturing was carried out in the baffled flask using a 1:5 (v:v) ratio of liquid to air to enhance the yield of vesicle production. The culture was shaken at 30°C for 5 h until cells reached the mid-log phase (OD600 ~ 0.6–0.8). Then, the required amount of isopropyl β-D-1-thiogalactopyranoside (IPTG) was added to a final concentration of 1 mM and the cultivation was continued for a further 20 h at 20°C to induce expression of the recombinant protein. Afterward, the bacterial pellet was precipitated by centrifugation at 5,000 × g (20 min) and cell-free culture supernatant was collected and filtered through a 0.45 μm filter and concentrated to 80 ml by ultracentrifugation (Ti98 rotor, Beckman-Coulter, California, United States). Lastly, OMVs were isolated by ultracentrifugation (Ti98 rotor, Beckman-Coulter, California, United States) at 170,000 × g for 2 h at 4°C. The purified OMVs were washed with phosphate-buffered saline (PBS) at 170,000 × g for an additional 2 h, followed by resuspending the pellet in 1 ml of PBS and passing through Detoxi-Gel endotoxin-removing columns (Pierce, Thermo Scientific, United States) and 0.20 μm cellulose acetate filters. The purified OMVs were stored at −20°C until use. The total protein concentration of OMVs was quantified using Bradford assay, and the bovine serum albumin was used as a standard.

Preparation of Recombinant AffiEGFR-OMVs

The gene fragment encoding His tag, G4S, myc tag, ZEGFR:1907 affibody, G4S, and GALA peptide was PCR-amplified using affibody forward (5′-GAGTGACTCCGAAGTCGGGGGCCGG -3′) and affibody reverse (5′-CTCTAGAATTATTTAGGAGCC GTGCATC-3′) primers using pMD18-T vector as a template. The amplified sequence was then cloned between KpnI and XbaI sites of the pET28a expression vector and the final construct was transformed and expressed in E. coli BL21 (DE3) strain. To express the recombinant protein, a 500 ml of bacterial culture supplemented with kanamycin was set and the protein expression was induced by adding IPTG (1 mM) at 37°C for 4 h. The bacterial pellet was then collected and lysed using lysis buffer (300 mM NaCl, 50 mM NaH2PO4, and 10 mM imidazole; pH8.0) and sonication (12 cycles of 20 s ON/OFF). Following centrifugation at 5,000 × g for 20 min, the supernatant was loaded onto the Ni-NTA agarose column (QIAGEN; Hilden, Germany) equilibrated with the same lysis buffer. After washing, the recombinant protein was eluted using the elution buffer (300 mM NaCl, 50 mM NaH2PO4, and 250 mM imidazole; pH8.0) and finally, imidazole was removed from the protein solution and replaced with PBS using an Amicon ultrafiltration system (3 kDa cutoff filter) (Millipore, Billerica, MA, United States). The concentration of the purified fusion protein was determined by the Bradford assay.

Characterization of the AffiEGFR-OMVs

Expression of the exogenous protein was detected by electrophoresis. Briefly, bacterial cells and OMV samples were suspended in lysis buffer (4% CHAPS, 7M Urea, 2M Thiourea, and 40 mM Tris-HCl) and boiled for 15 min in a loading buffer containing β-mercaptoethanol. After cooling to room temperature, samples were loaded onto a 10% polyacrylamide gel and separated electrophoretically. To visualize protein bands, SDS-PAGE gels were stained with Coomassie Brilliant Blue R-250 (BioRad, United States).

For Western blot analysis, bacterial cell lysates and OMV samples were separated by SDS-PAGE as described above and the protein bands were subsequently transferred to a PVDF membrane via semidry transfer. Membranes were blocked using skim milk in PBS (3% w/v) and the fusion protein band was detected by a mouse horseradish peroxidase (HRP)-labeled monoclonal antibody against the 6XHis-tag (1:1,000 v/v, Sigma-Aldrich, United States, A7058). For further verification, specific antibodies, including goat polyclonal anti-affibody primary antibody (1/4,000 v/v, Abcam, United Kingdom, ab50345) and HRP-conjugated anti-goat secondary antibody (Abcam, United Kingdom), were used. Bands were visualized using HRP substrate Clarity ECL kit (GE Health Care Life Sciences, Buckinghamshire, United Kingdom).

To confirm the surface distribution of ClyA-affibody-GALA in bacteria and OMVs, immune staining of the samples was performed and the samples were analyzed using flow cytometry. In brief, bacterial cells were centrifuged at 8,000 × g for 5 min and then washed with PBS at 8,000 ×g for another 5 min. Afterward, bacteria were blocked in PBS containing 3% (w/v) BSA for 15 min and incubated with anti-affibody antibody in 1% (w/v) BSA (1:500) for 1 h. Following washing, samples were incubated with FITC -conjugated secondary antibody (1:2000) (Abcam, United Kingdom) for 30 min. Flow cytometry analysis was performed using the CyFlow® SL machine (Partec, Munster, Germany). For OMVs, at the end of each step, OMVs were collected using a 50 kDa cutoff ultrafiltration tube (Millipore, Billerica, MA, United States) and centrifugation at 5,000 × g for 30 min (Huang et al., 2016).

Determining the Size and Morphology of the AffiEGFR-OMVs

Transmission electron microscope (TEM) analysis was performed for structural analysis of vesicles. For this purpose, fresh non-
targeted and EGFR-targeted OMVs (modified OMVs, mOMVs) (250 µg/ml) were resuspended in 3% glutaraldehyde with the ratio of 1:1 to fix them. Next, one drop of this solution was mounted on a Formvar coated grid. Samples were then negatively stained with 2% uranyl acetate for 2 min and air-dried for 1 hour. Upon washing with distilled water, the completely dried copper grids were examined under a transmission electron microscope Zeiss EM900, 80 kV (Germany), to assess the size and morphology of OMVs.

**Analysis of Size Distribution of OMVs**

Size distribution of non-targeted OMVs and the affiEGFR-OMVs was measured by dynamic light scattering (DLS) using a ZetaSizer Analyzer (Malvern Instruments Ltd. Nano-ZS ZEN3600, United Kingdom) equipped with a 5 mW HeNe laser and operating at an angle of 173°. To detect Z-average size and polydispersity index (PDI) of the OMVs, the OMV frozen samples were thawed at room temperature and diluted to 50 µg/ml (total protein concentration) in PBS. Z-average defines the mean diameter of the vesicles in nm (d.nm), while PDI describes the particle size distribution. Tracing analysis was performed in three independent runs for each sample in single-use polystyrene zeta cell DTS1060 with a path length of 10 mm by measuring the backscattering intensity at 25°C. Scattering light detected at 173° was automatically adjusted by laser attenuation filters. The software used to collect and analyze the data was the Zetasizer software version 7.01. Size distribution by intensity was preferred to measurements by number or by volume to have more reproducible results.

Furthermore, the alteration in size and PDI of affiEGFR-OMVs reflecting vesicles stability was tested during storage for a period of 3 days at 4°C.

**Tyndall Effect**

The Tyndall effect was applied to verify the existence of OMVs as nanoparticles in the solution using a red laser pointer as the light source. A visible light beam path can be observed in the nanoparticle solution due to Tyndall scattering.

**Monitoring the Specific Binding of the AffiEGFR-OMVs Using Enzyme-Linked Immunosorbent Assay**

Enzyme-linked immunosorbent assay (ELISA) was carried out to explore the specificity of the engineered OMVs for EGFR receptors according to a previously described protocol with some modifications (Kim et al., 2012). Briefly, 100 µL of EGFR protein (5 µg/ml) (Abcam, United Kingdom) and bovine serum albumin (BSA) (5 µg/ml in PBS) were coated onto 96-well plates (SPL, Korea) and incubated at 4°C overnight. Following removal of the coating solution, 200 µL of blocking buffer containing 2% of BSA was added and further incubated for 2 h at 25°C. Afterward, the plates were washed four times with PBS containing 0.1% of Tween-20 and exposed to 100 µL of the OMVs or affiEGFR-OMVs at different concentrations (5–150 µg/ml) and incubated for 2 h at 25°C. The affiEGFR-OMVs were then detected using 100 µL of goat polyclonal anti-affibody primary antibody (1/4,000 in PBST), followed by four times washing and incubating with horseradish peroxidase (HRP)-conjugated secondary antibody. The immunoreactivity was observed using the chromogenic HRP substrate 3,3′,5,5′-tetramethylbenzidine (TMB) (Abcam, United Kingdom) and the absorbance was measured at 450 nm. Finally, the function of the engineered OMVs was compared with the affiEGFR protein (0.1–10 µg/ml).

ELISA was also performed with cancer cell lines, MDA-MB-468 (EGFR-positive) and HEK293T (EGFR-negative) cell lines were grown in a DMEM medium containing 10% FBS. Cells (10^6/ml) were lysed by sonication (15 cycles: 10 s on/10 s off) at 80 A and then 100 µL of the cell lysate was coated onto each well (Banisadr et al., 2018). Upon blocking and washing, coated wells were incubated with 100 µL of the affiEGFR-OMVs and OMVs at 55 µg/ml as well as affiEGFR (3.5 µg/ml) and Cetuximab (Erbitox®, Merck) (1.5 µg/ml) as the positive control. HRP-conjugated anti-human secondary antibody (Cytomatin gene, Isfahan, Iran) was applied to detect Cetuximab binding.

**Cell Binding Assessment by Flow Cytometry**

Cell specificity and binding capacity of the affiEGFR-OMVs were examined by flow cytometry as described before (Zarei et al., 2014). In brief, 5×10^5 cells of each of MDA-MB-468 and HEK293T were spun down at 800×g for 5 min. Cells were resuspended in 100 µL of FACS buffer (PBS, 5% FBS) and incubated with 25 µg of OMVs and affiEGFR-OMVs or 1.5 µg of the affiEGFR for 2 h at 4°C. Following washing two times with FACS buffer and blocking, cells were incubated with 100 µL of anti-affibody antibody (1/500) for a further 2 h at 4°C, then stained with FITC-conjugated secondary antibody (1/2000) in the dark for 30 min at 4°C, and finally resuspended in PBS. The fluorescent intensity of the cells was measured by flow cytometry. All samples were compared to negative control. For the negative control, the cells were processed and stained in the same manner with anti-affibody and FITC-conjugated secondary antibody, except for incubating with OMVs or affiEGFR. To quantify the difference in cell binding, the mean fluorescence intensity was calculated for all the treatments.

**Competitive Binding Assay by Flow Cytometry**

The specific binding of the modified OMVs was more investigated in the presence of the EGFR competitors. For this goal, 5×10^5 cells of EGFR-positive MDA-MB-468 cells were pretreated with an excess amount of EGF (7.5 µg) or Cetuximab (186.5 µg) in 200 µL of FACS buffer (equal to 12.5 µM) for 90 min at 4°C. Having washed the cells, they were then treated with 25 µg of OMVs or affiEGFR-OMVs for a further 90 min at 4°C. Anti-affibody antibody and FITC-conjugated secondary antibody were applied as previously described. The fluorescent intensity of the cells was measured by flow cytometry.

The binding specificity of the affiEGFR-OMVs was also examined with the increasing concentrations of EGF as an EGFR competitor. To do it, MDA-MB-468 cells (5×10^5 cells/200 µL per tube) were incubated with 25 µg of affiEGFR-OMVs in the presence of 15 ng to 7.5 µg (3.25 nM–12.5 µM final
concentration) of EGF for 2 h at 4°C. Anti-affibody and FITC were used for staining cell-bound affiEGFR-OMVs. MFI was recorded and % of cell binding of affiEGFR-OMVs + EGF tests was calculated relative to affiEGFR-OMVs alone.

**Evaluation of EGF Receptors Expression and Phosphorylation by Western Blotting Analysis**

To detect expression of EGFR in MDA-MB-468 and HEK293T cells, the cells were seeded at 2.5×10⁶ in 6 well plates and incubated at the standard growth culture for 24 h. For the EGFR stimulation test, MDA-MB-468 cells were plated and treated with affiEGFR-OMVs (250 μg/ml) or EGF (100 nM) on the next day following overnight serum starvation. The cells were then lysed using RIPA lysis buffer (Sigma-Aldrich) containing protease inhibitors. The protein concentration was determined using the Bradford protein assay and protein samples were separated by 10% SDS-PAGE electrophoresis. Western blotting analysis was then performed as described before. Images were quantified using the ImageJ 1.4.3.67 (NIH software). The protein content was normalized to the level of β-actin. The antibodies used were as follows: EGFR (1/1,000, orb225296, Biorbyt, United Kingdom), p-EGFR (1/200, SC-81488, Santa Cruz Biotechnology, United States) and β-actin (1/1,000, 4967S, Cell Signaling, United States).

**Monitoring the Cell Binding and Cell Uptake of AffiEGFR-OMVs by Confocal Microscopy**

To visualize the cell binding of OMVs, confocal microscopy was applied (Gujrati et al., 2014). In a few words, 1.5×10⁵ of MDA-MB-468 and HEK293T cells were seeded on 8-well glass slides (SPL Life Sciences, Korea) in a DMEM medium containing 10% FBS and antibiotics for 24 h to reach 60% of confluency. Cells were then fixed with paraformaldehyde (PFA, 3.7% in PBS) for 15 min, blocked by 2% of BSA for 1 h at room temperature, and then further incubated with the affiEGFR-OMVs (25 μg) for 2 h at 4°C. Samples were sequentially exposed to anti-affibody primary antibody (1:500) and FITC-labeled secondary antibody (1:2,000). Cells were finally evaluated under a confocal microscope (Olympus Fluoview TM FV 1000, Olympus, Japan).

For tracing the cellular uptake of OMVs, MDA-MB-468 cells at 60% of confluency were exposed to the OMVs and affiEGFR OMVs (25 μg) for 2 h at the standard growth culture. After being washed with PBS, cells were fixed in 3.7% of PFA at room temperature for 10 min. Fixed cells were then washed and permeabilized by 0.1% Triton X-100 for 10 min. Avoiding nonspecific interaction of antibodies, cells were treated with 3% (w/v) of bovine albumin serum (BSA) in PBS for 1 h at room temperature. Cells were finally incubated with anti-affibody primary antibody and FITC-labeled anti-goat secondary antibody. The nuclei were stained with propidium iodide (PI, 1 μg/ml) (Sigma-Aldrich, MO, United States) and cells images were taken by the confocal microscope.

To investigate the uptake of affiEGFR-OMVs by MDA-MB-468 cells, EGFR-overexpressing cells were initially incubated with EGF (7.5 μg) or Cetuximab (186.5 μg) for 2 h in a standard culture medium. Following washing, cells were exposed to 25 μg of OMVs or affiEGFR-OMVs and incubated for a further 2 h at 37°C. The procedure was similar to that described for tracing cell uptake. Finally, the treated cells were evaluated using a confocal microscope.

**Measuring the AffiEGFR-OMVs Using the Gel Clot Limulus Amebocyte Lysate Assay**

Endotoxicity of affiEGFR-OMVs in both the intact and lysed (with 0.5% of sodium deoxycholate) forms was evaluated using the commercial gel clot LAL kit (PYROTELL, Associates of Cape Cod Inc. United States). Serial dilutions of affiEGFR-OMVs and its lysate (250 down to 7.81 μg/ml) were applied in this test, and endotoxin activity was assayed as per the manufacturer's instructions in duplicate. Control standard endotoxin (CSE) (E. coli strain O111:B4, 0.5 EU/mL) and LAL reagent water (LRW), provided by the Associates of Cape Cod Inc., were used as positive and negative controls, respectively.

**Sterility and Hemolytic Activity of the AffiEGFR-OMVs**

To assess sterility of the affiEGFR-OMVs, OMV preparations were plated on LB-agar plates and grown overnight at 37°C. Cytolytic or hemolytic activity assay was performed using horse blood agar plates. To do this, the affiEGFR-OMVs-derived (500 μg/ml) and its parent strains (transformed ΔmsbB/ΔpagP W3110) were plated on the horse blood agar plates and incubated at 37°C overnight. β-Streptococcus was also plated as a positive control. The next day, plates were analyzed for any clear zone as a result of red blood cells lysis. A liquid hemolysis assay was also performed to show the hemolysis activity quantitatively. To this end, human erythrocytes were washed and diluted with a ratio of 2:100 in PBS. Aliquots of the washed erythrocytes were then transferred to a v-bottom 96-well plate and subjected to affiEGFR-OMVs (6.25–400 μg/ml) for 1 h at 37°C. Upon centrifugal sedimentation of the cells and debris at 2000 rpm for 5 min, the supernatant hemoglobin was quantified by spectrophotometric detection at 540 nm. PBS and deionized water were used as negative and positive controls, respectively. Hemolysis activity was reported relative to the erythrocytes lysed in deionized water.

**Determining Cell Viability Following Outer Membrane Vesicles Exposure**

Cell viability was measured following OMVs exposure via MTT assay in the MDA-MB-468 and HEK293T cell lines. In short, a total of 1×10⁵ cells were seeded in 96-well plates overnight and treated with both OMVs and the affiEGFR-OMVs (25–400 μg/ml) for 4 h. The medium was then refreshed and the cells were further incubated for 72 h in a standard growth condition. To confirm the nontoxic effect of OMVs, the percentage of cell viability was calculated. Cisplatin (Sigma-Aldrich, MO, United States) was also applied as a positive control.
THP1 Cell Stimulation
The procedure for this assay was as described previously with certain modifications (Widdrington et al., 2018). Briefly, THP-1 cells were grown as a suspension culture in RPMI-1640 medium containing 10% FBS. Cells were then exposed to 200 nM of phorbol myristate acetate (PMA) for 48–72 h to induce differentiation. Afterward, the obtained adherent cells were treated with afEGFR-OMVs (25–400 μg/ml) along with PBS and LPS (100 ng/ml) (Sigma-Aldrich, MO, United States) as negative and positive controls, respectively. Following a 24 h incubation, human TNF-α was quantified using ELISA (Quantikine HS, United States) as per the manufacturer’s instructions.

Statistics
All statistical analyses were performed using GraphPad Prism 8 (GraphPad Software, La Jolla, CA, United States). Differences were considered significant if the p value was <0.05. All graphed values represent the mean, and the error bars show standard error. One-way analysis of variance (ANOVA) followed by post hoc Tukey’s test was used for intergroup comparisons.

RESULTS
Recombinant ClyA-affiEGFR-GALA Was Expressed on W3110 E. coli
The ΔmsbB/ΔpagP W3110 E. coli K12 strain is a nonpathogenic strain harboring two mutations in msbB and pagP genes to highly reduce endotoxin activity (Lee et al., 2011). ClyA-affiEGFR-GALA construct (Figure 1A) was transformed into this strain to prepare the affiEGFR-OMVs with the least cytotoxic effect.

As illustrated by SDS-PAGE, a clear protein band of ~50 kDa, corresponding to the full-length ClyA-affiEGFR-GALA along with tags, was detected in the whole-cell lysate of recombinant W3110,
indicating that the fusion protein had efficiently been expressed in W3110 cells. Furthermore, the presence of the fusion protein in the OMVs derived from the engineered ΔmsfB/ΔpagP W3110 samples was confirmed by immunoblotting using anti-6XHis-tag (data not shown) and anti-affibody antibody (Figure 1B). Detection of a reacting band of about 50 kDa further confirmed the successful expression of the ClyA-affiEGFR-GALA fusion protein in the OMVs.

Next, to verify whether the fusion protein was present on the surface of OMVs, the intact W3110 cells and OMVs were subjected to anti-affibody antibody treatment and analyzed by flow cytometry. Our findings confirmed the presence of affiEGFR-GALA on the surface of OMVs. In other words, cells and OMVs displaying affiEGFR were brightly fluorescent, while no fluorescence was detected for the untransformed cells and OMVs (Figure 1C). To validate these findings, we also expressed and then purified the affiEGFR recombinant protein (16 kDa) as a positive control in BL21 DE3 (Figure 1D).

Taken together, using genetic engineering techniques, the affiEGFR-GALA was successfully presented on the surface of ΔmsfB/ΔpagP W3110-derived OMVs via fusion to ClyA.

Characterization of the Engineered Outer Membrane Vesicles

Transmission Electron Microscopy

Morphological and structural alterations of the engineered OMVs were examined by TEM. The findings exhibited spherical nanoscale vesicles, which in comparison to non-targeted OMVs, no significant difference in morphology was detected in the modified OMVs (affiEGFR-OMVs). These results suggest that the association of ClyA-affiEGFR-GALA in the engineered OMVs had no apparent effect on the size of the particles (Figure 2A).

Dynamic Light Scattering and Tyndall Effect

The identical size distribution of the OMVs and affiEGFR-OMVs was confirmed by dynamic light scattering analysis (Figure 2B). As reported in Table 1, there was no significant difference (p > 0.05) in terms of polydispersity index (PDI), maximum peak (nm), and Z-average (d.nm) between two types of OMVs. These results were in parallel with the TEM findings confirming that incorporation of a heterologous protein did not alter the size of the affiEGFR-OMVs. To verify the stability of the OMVs, the frozen OMVs were thawed and the above parameters were determined on three consecutive days at 4°C. As indicated in Table 2, no significant alteration was observed in terms of PDI and Z-average.

Moreover, to demonstrate the colloidal feature of the OMVs solution, the Tyndall effect was evaluated in the samples. The Tyndall effect is the phenomenon indicating the divergence of a light beam when it passes through a colloidal dispersion and a portion of the light is scattered. As it can be seen from Supplementary Figure S1, the PBS buffer sample has no obvious Tyndall effect, while the OMVs solution sample has a strong Tyndall effect confirming the presence of OMVs.

AffiEGFR-OMVs Specifically Bound to Epidermal Growth Factor Receptor-1 Protein in ELISA Test

AffiEGFR-OMVs have to identify EGFR protein in ELISA. For further verification, affiEGFR protein was used as a positive control. As shown in Figure 3A, both affiEGFR-OMVs and affiEGFR interact with the EGF receptor in a concentration-dependent manner; i.e., the higher the affiEGFR-OMVs concentration, the greater the strength of binding. It is worth mentioning that the graph in Figure 3A finally reaches a saturation plateau. As expected, affiEGFR was effective even at a low applied concentration. Interestingly, no absorbance was detected for the OMVs even at the highest applied concentrations (Figure 3A). Our calculated Kd values were 86.41 and 2.845 μg/ml for the engineered OMVs and affiEGFR, respectively. Based on the Kd values, it is suggested that 1 μg of the affiEGFR-OMVs includes 32 ng of affiEGFR corresponding to about 3% of the total protein.

ELISA Assay of Cell Lysate Confirmed AffiEGFR-OMVs Specific Binding

For further validation, an ELISA test was also carried out on the cell lysates. Both affiEGFR-OMVs and affiEGFR interacted with MDA-MB-468 cells. A high and reliable concentration (~EC50) was used for satisfactory results. The results showed that the absorbance values for affiEGFR and affiEGFR-OMVs interacting with MDA-MB-468 cell lysate were significantly higher than those for the HEK293T cell lysate. As expected, HEK293T cells did not interact with either affiEGFR-OMVs, affiEGFR, and Cetuximab owing to their lack of receptor (Figure 3B). These results are in line with our immunoblotting findings verifying no EGF receptor expression in HEK293T cells (Supplementary Figure S2). Moreover, no significant difference in terms of OD values was detected following incubation of both MDA-MB-468 and HEK293T cells with non-targeted OMVs. In contrast, Cetuximab as a positive control exhibited a high OD value at the concentration applied in MDA-MB-468 cells.

In summary, the above results indicate specific binding of affiEGFR-OMVs to the cells expressing EGFR receptors due to the presence of the ZEGFR affibody.

AffiEGFR-OMVs Bound to EGFR-Overexpressing MDA-MB-468 Cells

The binding property of the affiEGFR-OMVs was also compared to that of non-targeted OMVs in MDA-MB-468 and HEK293T cells using flow cytometry (Figures 4A,B). In parallel, affiEGFR was utilized in this assay as a positive control. As illustrated in the results, the shift in fluorescence intensity for the affiEGFR-OMVs and affiEGFR is well associated with the expression level of the receptor on the MDA-MB-468 cell surface; i.e., cells having a higher EGFR expression level revealed a greater shift than the non-EGFR-expressing HEK293T cell line. The non-targeted OMVs exhibited no binding to HEK293T and MDA-MB-468
cells ruling out any nonspecific binding of OMVs to the tumor cells under investigation. These results are in agreement with the ELISA data addressing the specific binding of the affiEGFR-OMVs to the EGF receptor.

We also found no detection of affiEGFR-OMVs and affiEGFR when EGFR-negative HEK293T cells were used since neither a fluorescent shift nor an enhancement in intensity was detected relative to the negative control under the same conditions. Interaction between the engineered OMVs and MDA-MB-468 cells was further investigated by confocal microscopy after co-culturing of the cells with 25 µg of the affiEGFR-OMVs for 2 h at 4°C. As it can be seen in Figure 5A, the affiEGFR-OMVs clearly bound to the surface of MDA-MB-468, whereas no binding was observed for HEK293T cells, used as the EGFR deficient cells. The findings of the confocal microscopy were in parallel with those of our previous assays, confirming that the affiEGFR-OMVs can selectively and effectively target EGF receptors.

**Internalization of the AffiEGFR-OMVs Into EGFR-Overexpressing MDA-MB-468 Cells**

To further study the uptake of the OMVs by the cancer cells, MDA-MB-468 were treated with the non-targeted OMVs and affiEGFR-OMVs for 2 h at 37°C. Confocal microscopy revealed the cellular entry of the affiEGFR-OMVs, with red and green fluorescence pointing to the location of cell nuclei and OMVs, respectively, while no fluorescence was observed in the MDA-MB-468 cells treated with the non-targeted OMVs (Figure 5B).

**AffiEGFR-OMVs Compete With Epidermal Growth Factor and Cetuximab for Binding and Uptake by MDA-MB-468 Cells**

To further investigate the specific binding of the affiEGFR-OMVs, EGFR-specific ligands, EGF, or Cetuximab was applied to compete with the affiEGFR-OMVs for binding to EGFR-overexpressing MDA-MB-468 cells. The flow cytometric data verified a specific interaction between affiEGFR-OMVs and MDA-MB-468 cells. As evidenced in Figure 6A, pretreatment with an excess amount of EGF or Cetuximab heavily blocked affiEGFR-OMVs binding to the target cells (8.20 and 6.04 MFI, respectively), while no significant fluorescent shift was observed in the case of OMVs. Moreover, co-incubation with 3.25 nM – 12.5 μM of EGF resulted in a decrease of fluorescent intensity from 89.43 to 9.2% (Figure 6B). Indeed, these data indicate a gradual reduction in the binding ability of affiEGFR-OMVs to the receptors with increasing amounts of EGF, further supporting the specific binding to EGF receptors.

We also assessed the target-specific delivery of the affiEGFR-OMVs. To do it, EGF or Cetuximab pretreated MDA-MB-468 cells were examined with a fluorescence confocal microscope. As evidenced in the data, a significant reduction in green fluorescence intensity was visualized following the pretreatment.

**TABLE 1** | Size distribution parameters of OMVs and modified OMVs (mOMVs) determined by DLS*.  

| Maximum peak (nm) | Z-Average (d.nm) | PDI |
|-------------------|------------------|-----|
| OMVs 192.26 ± 14.55 | 136.26 ± 38.15 | 0.417 ± 0.044 |
| mOMVs 186.36 ± 25.98 | 135.76 ± 30.33 | 0.370 ± 0.043 |

*Values were expressed as mean ± SD from three independent runs.

**TABLE 2** | Size and PDI value of vesicles of mOMVs stored at 4°C during 3 days.  

| Day | PDI  | Z-Average (d.nm) |
|-----|------|------------------|
| Day 1 | 0.369 | 167.4            |
| Day 2 | 0.372 | 228.2            |
| Day 3 | 0.426 | 238.9            |

**FIGURE 2** | Characterizing the engineered OMVs. (A) Transmission electron microscopic observation of the OMVs (left) and modified OMVs (mOMVs) (right). The bar indicates 150 nm. (B) Dynamic light scattering confirmed the size distribution of OMVs.
of MDA-MB-468 cells with an excess amount of the competitors, EGF and Cetuximab (Figure 6C).

Overall, the competition results further demonstrated the target-specific anti-EGFR-OMVs delivery to the cells.

No Epidermal Growth Factor Receptor-1 Activation Following Anti-EGFR-OMVs Treatment

Autophosphorylation of EGFR as the primary transformation that happens upon ligand induction is a crucial characteristic of EGFR activation (Lemmon and Schlessinger, 2010). To examine if the anti-EGFR-OMVs activate EGFR receptors, phosphorylation of EGFR was monitored following treatment of MDA-MB-468 cells with anti-EGFR-OMVs and EGF as a positive control. Western blotting results using EGFR phosphorylation site-specific antibody (Tyr1068) exhibited a significant band indicating expression of the phosphorylated EGFR in the EGF-treated samples. In contrast, no phosphorylated protein expression level was detected in the anti-EGFR-OMVs treated cells (Figure 7). These findings confirmed that OMVs presenting affibody target cancer cells with no receptor stimulation effect.

Safety Assessment of the Engineered Outer Membrane Vesicles

Besides the efficacy of targeting, the safety issue is a pivotal concern in the development of nanomedicine, where a bacterium-derived
product is utilized. Since OMVs consist of a large portion of LPS activating toll-like receptors (TLRs), which in turn provokes an inflammatory response (Kuehn and Kesty, 2005), we thus evaluated OMV-induced inflammatory response by assessing TNF-α level and cytotoxicity in vitro. We also performed hemolysis and sterility studies and measured the endotoxin levels as well to assure the biocompatibility of the OMVs.

The Engineered OMVs Showed No Endotoxicity
Findings from the gel clot LAL test showed the absence of a stable solid clot in the test tubes at the end of reactions confirming the lack of LPS for affiEGFR-OMVs and its lysate at all the concentrations used. The lack of endotoxin activity in the intact OMVs and the OMVs lysate, in which the lipid-A component of LPS is exposed, confirmed the exploitation of the LPS-modified ΔmsbB/ΔpagP W3110 strain in the current study.

No Bacterial Growth Was Observed for the Engineered OMVs
The sterility of the purified OMVs was determined by plating the affiEGFR-OMVs on LB-agar plates and incubating at 37°C overnight. The absence of the bacterial colonies proved that the OMV products were bacteria-free (Figure 8A).

The Engineered OMVs Revealed No Hemolytic Activity
To validate the hemolytic activity of the affiEGFR-OMVs, the blood agar plated OMVs were prepared under the standard incubation conditions. No hemolysis was visualized upon plating the affiEGFR-OMVs and its origin bacteria, while clear zones were seen owing to the β-streptococcus strain culturing as a positive control (Figure 8B). The data from the quantitative liquid hemolytic assay supported our findings and displayed no considerable difference in erythrocyte hemolysis compared to PBS as the negative control (Figure 8C). These observations indicated that ClyA fusion protein is in an inert state and the affiEGFR-OMVs are safe enough to be used as a nanocarrier.

The Engineered OMVs Had No Effect on the Cell Viability
Our data on the MTT assay on HEK293T and MDA-MB-468 cell lines revealed no significant alteration in terms of viability following transfection with the affiEGFR-OMVs compared to the PBS-treated cells, while cell viability was reduced to about 50% following Cisplatin treatment as a positive control. In other words, the normal appearance of the cells in both treatments implies no cytotoxic effect associated with the affiEGFR-OMVs (Figure 8D).
No Immunogenicity for the Engineered OMVs

Based on a previous study reporting on the potent stimulatory activity for LPS in the production of TNF-α in THP1 cells, we next investigated the stimulation of the immune system by affiEGFR-OMVs in these cells and found that the affiEGFR-OMVs caused a slight increase in TNF-α level in human monocyte THP1 cells compared to cells induced with LPS (Figure 8E).

The desired findings from our in vitro assays pointed out the safety and biocompatibility of the engineered OMVs as a drug carrier in cancer research.

DISCUSSION

Targeted cancer therapy is one of the most cost-effective strategies to prevent severe and often long-lasting side effects of chemotherapy (Miller et al., 2016). Hence, the need for exploring and developing novel targeted nanoparticle delivery platforms remains the main subject to achieve more effective and reliable therapies. In this context, OMVs derived from genetically manipulated bacterial strains offer great potential for cancer targeting and are introduced as valuable drug carriers in cancer therapy (Gujrati et al., 2014). These particles are efficient in shielding their content and protect them against proteases, leading to an increased circulating half-life of the nanodrugs (Gujrati et al., 2014; Kim et al., 2017).
Furthermore, by appropriate engineering, OMVs can target the specific cancer cells, which in turn reduce the unwanted side effects of the associated drugs (Kim et al., 2017). Given these data and considering that EGF receptors have been the subject of numerous cancer studies, the work presented here exploits the bacterial OMVs in targeting EGF receptors in triple-negative breast cancer cells. Triple-negative breast cancer (TNBC) has an aggressive feature, and so far, there is no available agent to target this type of tumor (Engebraaten et al., 2013; Cao et al., 2019; Damaskos et al., 2019). This motivated us to prepare the surface-modified OMVs by genetic fusion of ZEGFR:1907 affibody to the C-terminus of ClyA to increase the chance of presenting a properly folded affiEGFR protein. As previous studies have demonstrated (Kim et al., 2008; Chen et al., 2010; Huang et al., 2016), the addition of ClyA as a leader sequence to the N-termini of the affibody assures the construct to be presented on the surface of the OMVs. This approach has been successfully employed in other studies using either OmpA or ClyA depending on the location of the proteins, i.e., into the lumen or on the surface of OMVs (Fantappie et al., 2014). In this line, we prepared the engineered OMVs for proof of concept of applying OMVs not only as an effectual antigen delivery system but also as a targeted nanocarrier.

Interestingly, the small size of the ZEGFR:1907 affibody (~7 kDa) is an advantage to keep the size and morphology of OMVs unchanged. This was confirmed by DLS and TEM data. Apart from the small size of the ZEGFR:1907 affibody, the selectivity and high affinity to EGF receptors are the most important features of this molecule. ZEGFR:1907 is the second-generation of EGF-specific affibody molecules, demonstrating a desirable tumor localization with no cross-binding to other growth factor receptors (Tolmachev et al., 2009). Previous studies have found...
that this affibody could be an appropriate candidate for targeted imaging in EGFR-expressing cells, including A431 and HCC tumors (Zhao et al., 2013). Consistently, our ELISA findings using EGFR protein revealed a satisfying affinity for both the purified Z_{EGFR} affibody-GALA (K_{d}: 2.845 μg/ml) and Z_{EGFR} affibody presented on the surface of OMVs (K_{d}: 86.41 μg/ml). From the K_{d} values, we speculated that the affi_{EGFR}-OMVs contain about 3% of affibody-GALA out of the total OMV proteins, which surprisingly is similar to those estimated by Western blotting analysis (ranging from 1 to 5%) (Fantappie et al., 2014).

Furthermore, this amount of affibody protein was detected when EGFR-negative cells were used, confirming the anti-EGFR engineered OMVs as an alternative approach to assure cell specificity. The results demonstrated that the nonspecific cellular binding is low for the modified OMVs, providing further insight into the EGFR receptor-mediated cellular interaction. Moreover, our findings revealed that binding capacity of the engineered OMVs gradually reduced when increasing concentrations of EGFR was added. These results were in agreement with our previous experiments in further confirming the targeted delivery system.

Since triple-negative breast cancer is known to overexpress EGFR and the EGF receptor is a well-established cancer therapy target (Seshacharyulu et al., 2012), using E. coli OMVs and the ClYl displaying system, we introduced a platform with a capability of specifically targeting triple-negative breast cancer, which can be further employed for cancers overexpressing EGF receptors. It is worth mentioning that several studies have proved that the expression of EGFR in triple-negative breast carcinoma is significantly higher than that of normal cells (Tang et al., 2012). However, the potential toxicity of the therapeutics targeting EGFR toward normal tissues is still challenging. This encouraged us to reveal the specificity of our construct toward the triple-negative breast cancer cells. Among a series of experiments conducted, immunofluorescence imaging of the MDA-MB-468 cells treated with the affi_{EGFR}-OMVs presented an alternative approach to assure cell specificity. The data obtained indicated that the anti-EGFR engineered OMVs strongly bind to EGFR-overexpressing target cells, while no binding was detected when EGFR-negative cells were used, providing further evidence that this adherence was via interaction between Z_{EGFR} affibody and the EGF receptor. Interestingly, we also verified that no EGF activation occurs following the adherence of the targeted OMVs to EGFR receptors by measuring the level of phosphorylated EGFR expression. Furthermore, a critical concern when applying OMVs in cancer therapy is intracellular delivery. To this end, images taken by confocal microscopy confirmed the efficient uptake of the engineered OMVs by the EGFR-overexpressing cells. Conversely, the non-targeted OMVs were unable to enter the cancer cells. Since the nonspecific process can cause increased OMVs uptake, we also captured confocal images of the target cells pretreated with EGF or anti-EGF mAb Cetuximab. The images validated the co-internalization of the modified OMVs with EGF receptors and exhibited that the modified OMVs competed with both Cetuximab and EGF in binding to EGFR and cellular uptake. These findings were in parallel with the report by Kim et al., indicating the incorporation of EGF on the surface of OMVs to efficiently bind to tumor cells expressing EGF receptors in vitro (Kim et al., 2017). However, a major concern in this study was the mitogenic and neoangiogenic properties of EGF. Recently, HER2 was selected as a target and anti-HER2 affibody expressed on the surface of OMVs was used for cancer-specific targeting due to its very high affinity and small size (Gujrati et al., 2014), which led us to design our engineered OMVs toward triple-negative breast cancer.

Of note, one of the major barriers in the cytosolic delivery of biomacromolecules is endocytosis; thus, efficiency to escape endosome seems to be important (Kakudo et al., 2004; Varkouhi et al., 2011; Burks et al., 2015; Niikura et al., 2015). To make sure of endosomal escape, GALA was fused to the C-terminus of the His tag-Z_{EGFR} fusion protein. Consistent with our study, a recent trial using a confocal laser scanning microscope (CLSM) showed the endosomal escape capability of a Z_{HER2} affibody displaying bio-nanocapsule following fusing with GALA on the surface of the particle (Nishimura et al., 2014). Indeed, we focused our attention on representing a potential model for a delivery system by genetically engineering OMVs equipped with GALA in which multiple parts would act in concert to accomplish an effectual and specific delivery platform to be used in EGFR-positive breast cancer therapy.

On the other hand, a key concern with the use of OMVs is the presence of LPS (Ellis et al., 2016; Vanaja et al., 2016). Since OMVs are released from the outer membrane of bacteria, they have intrinsic inflammatory potential owing to their LPS content (Kuehn and Kesty, 2005). In other words, an integral pro-inflammatory component of LPS, the hexa-acylated lipid-A, stimulates the immune system through activating toll-like receptors pathways (Ellis et al., 2010). Here, we used an E. coli W3110 strain carrying double mutations of the msbB and pagP genes, which is able to generate OMVs with only penta-acylated LPS. The endotoxic activity of the modified OMVs from this double mutant has been attenuated several times compared to the wild-type W3110 (Lee et al., 2011). Hence, our engineered OMVs are supposed to stimulate a minimum immunogenic and toxic response, avoiding the possible undesirable or even fatal effects during the treatment process (Gujrati et al., 2014; Alves et al., 2015).

Of interest, our in vitro immune-stimulating assessment revealed no significant increase in the level of TNFa even at high concentrations in THP1 cell culture media following incubation with the affi_{EGFR}-OMVs compared to LPS as a positive control. For further verification, the hemolytic activity of the engineered OMVs was compared to that of the original bacteria using blood agar plates, and the liquid hemolysis assay.
was simultaneously performed as well. The results indicated that ClyA-ZEGFR GALA fusion protein is non-hemolytic. Further support for our results is that ClyA, a protein known for its hemolytic activity, has a latent/silenced structural gene in *E. coli* K-12 so that under many tested laboratory conditions, it is phenotypically silent in *E. coli* K-12 (Oscarsson et al., 1999; Westermark et al., 2000; Kim et al., 2008). Interestingly, it was reported that the absence of functional ClyA expression in an *E. coli* host can facilitate the translocation of the recombinant ClyA-fusions to the outer membrane and the presentation of a fusion partner on the derived OMVs (Huang et al., 2016). In this study, surface localization of the ZEGFR GALA using ClyA as a leader protein was confirmed by immune fluorescence staining and flow cytometry.

Moreover, targeted OMVs are needed to rule out toxic side effects. Cell viability findings displayed no significant difference between cells incubated with the affiZEGFR-OMVs and PBS, confirming the biosafety of the engineered OMVs for our future design and development of OMVs-based studies to develop effective and well-tolerated chemotherapeutics.

Naturally occurring vesicles such as OMVs provide a number of therapeutic advantages, as addressed earlier (Gu et al., 2020); however, no clinical studies have yet identified OMVs as a drug delivery vehicle. Indeed, despite developments in the employment of the extracellular vesicles in clinical trials, many challenges are needed to be overcome prior to a successful therapeutic application. As a consequence of the aforementioned caveats, the trials are limited to a few cases. In this context, phase I clinical trials have been performed using tumor peptide/drug–loaded exosomes in patients with metastatic melanoma, advanced non-small cell lung cancer (NSCLC), colorectal cancer (CRC), and malignant glioma (Thomas Jefferson University Hospital, 2000; Escudier et al., 2005; Morse et al., 2005; Dai et al., 2008; Ohno et al., 2016). Moreover, two phases I of clinical trials have recently assessed the oral plexosome-based curcumin delivery to normal and cancerous colon tissues (James Graham Brown Cancer Center, 2000). In the case of OMVs, phase I and II clinical trials only demonstrated the protective effect of OMV-based vaccine against *N. meningitidis* (de Kleijn et al., 2000; Marsay et al., 2015; Zhang et al., 2019).

The findings of this study are the first step toward achieving a targeted drug delivery system, which paves the way for further investigation on verification in the relevant *in vivo* and clinical models.

**CONCLUSION**

In the light of the foregoing results, we concluded that the EGFR affibody can be directed onto the OMV surface via ClyA fusion. The success of targeting triple-negative breast cancer cells by the affiZEGFR–OMVs followed by the internalization of the vesicles with no cytotoxic, hemolytic, or immune-activating effects is an interesting finding. However, research concerning the application of OMVs in cancer therapy is just in its infancy.

**DATA AVAILABILITY STATEMENT**

The original contributions presented in the study are included in the article/Supplementary Material; further inquiries can be directed to the corresponding author.

**AUTHOR CONTRIBUTIONS**

ZS contributed to performing the experiments, data interpretation, and writing the manuscript. MM helped in data acquisition and analysis. SB was involved in design of bacterial experiments. VK supervised the genetic engineering experiments. MS designed and supervised the study plan and wrote the manuscript.

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**SUPPLEMENTARY MATERIAL**

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fphar.2021.719289/full#supplementary-material

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