CATHETER ABLATION

RESEARCH REVIEW

The Effects of Catheter Ablation on Permanent Pacemakers and Implantable Cardiac Defibrillators

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ABSTRACT. Catheter ablation is a procedure that is frequently performed in patients with cardiac implantable electronic devices. Here, we review all of the potential interactions that can occur among patients undergoing catheter ablation while having implantable cardiac electronic devices, and discuss the precautionary measures to minimize such interactions.

KEYWORDS. Catheter ablation, implantable cardiac defibrillators, permanent pacemakers.

Introduction

The use of cardiac implantable electronic devices (CIEDs) has witnessed a steady growth since the introduction of permanent pacemakers (PPMs) in the 1960s and implantable cardioverter-defibrillators (ICDs) in the 1980s. Meanwhile, over the past two decades, catheter-based ablation has emerged as an integral component of atrial and ventricular arrhythmia management. As a result, catheter ablations are becoming more often required in patients with previously implanted CIEDs. Cardiac electrophysiologists are, for instance, more likely to encounter patients with right ventricular or coronary sinus leads requiring a cavotricuspid ablation or ablation in the coronary sinus, respectively (Figures 1 and 2). The Heart Rhythm Society and the American Society of Anesthesiologists have recommended avoiding direct contact between ablation catheters and the CIED systems. However, these consensuses are more based on precautionary measures, rather than on convincing clinical data, as clinical studies evaluating interactions between CIEDs and catheter ablation catheters remain limited in number. Furthermore, prior studies can become quickly outdated as the technology associated with CIED and catheter ablation continues to rapidly evolve (for instance, with the introduction of improved shielding, filters and algorithms against electromagnetic interference). In this review, we discuss the various interactions that might occur between the two most common therapies in cardiac electrophysiology, and strategies for preventing adverse outcomes.

Potential interactions between cardiac implantable devices and catheter ablation

Various interactions have been reported between catheter ablation and CIEDs, depending on how close the contact between them is, and the type of energy that is used. While radiofrequency (RF) and cryotherapy are currently the two main forms of energy used during catheter ablation, RF is by far the most common ablation modality. As such, potential interactions between ablation catheters and CIEDs may include (1) the effects of RF current (typically 500 to 1,000 kHz) on CIED pulse generators, including electromagnetic interference (EMI) oversensing and the resulting inappropriate sensing, as well as pacing and/or delivery of therapies in the form of inappropriate antitachycardia pacing and defibrillation shocks for ICDs; (2) transvenous lead dislodgment because of catheter manipulation; and (3) alterations in pacing, sensing or impedance parameters because of ablation completed in close vicinity or in direct contact with the lead.

1) Effects on the pulse generator

The majority of conventional pacemaker pulse generators are not adversely affected by exposure to RF energy during ablation, and those that are affected are done so transiently and often exhibit sensing-related issues.
The majority of the effects during RF energy application are related to EMI, and may include: noise reversion mode with asynchronous pacing, oversensing of EMI with rapid tracking, spurious arrhythmia detection, mode switch or pacing inhibition, inappropriate pacing and/or transient reset to elective replacement interval. If rate response is on, pacing at the upper sensor rate may occur, since EMI can alter intrathoracic impedance measurements. Fortunately, modern pulse generators and leads are less sensitive to EMI due to the development of improved shielding, and we typically do not see adverse interactions. It is also important to consider that programming devices to address asynchronous pacing during catheter ablation can be associated with a low but possible risk of ventricular fibrillation/tachycardia, because of the pacing on the T-wave that occurs during the vulnerable ventricular period and/or short-long-short sequence. Meanwhile, cryoablation has not been reported to cause interference with CIED pulse generator function.

Robotic ablation with remote magnetic catheter navigation (RMN) (Niobe® system, Stereotaxis, St. Louis, MO, USA) can be associated with EMI, since it uses magnetic fields to move an ablation catheter. One in vitro study tested 121 explanted pacemakers and defibrillators not connected to leads at maximal field strength and found that 5% of the devices exhibited transient changes (the pacemakers only), but could be reprogrammed after being removed from the magnetic field. RMN, however has not been shown to adversely impact CIED function in vivo.

In the case of subcutaneous defibrillators, to date there have been no reports of significant interactions with catheter ablation, though its use in the United States is rapidly increasing. Since the pulse generator and lead system are entirely subcutaneous, the anticipated potential interaction is EMI. Therefore, ICD therapy should be disabled prior to delivering RF energy. Another novel technology that is being utilized is the leadless pacemaker. In a recent study, five patients underwent leadless transcatheter pacemaker implantation followed by atrioventricular (AV) nodal RF ablation (for uncontrolled AF) without any reported interactions. This is the only study to date that has evaluated RF ablation in patients with leadless pacemakers.

2) Lead dislodgement

In addition to electronic interference, there is always a risk of mechanical micro- or macrodislodgment occurring in patients with implanted devices who are undergoing catheter ablation, especially among recently implanted leads. In a study that assessed the effects of RF during atrial fibrillation ablation among 86 patients with CIEDs, there were no direct RF-related adverse effects on lead function. However, atrial lead dislodgement occurred in two patients with newly implanted leads of less than 6 months. There is a possibility that lead dislodgment might become more common with the current trend of fluoroscopy-free ablation procedures. However, other clinical studies have failed to show lead dislodgement...
secondary to RF ablation. Overall though, the risk of mechanical dislodgment remains possible if enough traction is applied on the lead. To minimize this complication, it is recommended that the process of lead maturation be allowed to occur. Lead maturation is an inflammatory reaction that is produced following lead tip contact with endocardium that results in distal electrode encapsulation within the myocardial tissue. This process typically occurs 2–6 weeks after implantation, and results in a more stable lead with the electrode embedded in the cardiac tissue. However, it is generally accepted that there is an increased chance of lead dislodgement up to 3 months after implant. Therefore, we recommend allowing for a minimum of 6 weeks after CIED implantation, but ideally 3 months, to pass before an ablation procedure is performed.

3) Effects of ablation close to or in direct contact with a CIED lead

Effect on lead/tissue interface. In certain cases, myocardial thermal lesions may occur at the tip of the pacemaker and ICD leads from transmitted RF energy applied to the distal electrode. Therefore, tissue alterations at the lead/myocardial tissue interface may result in decreased sensing or an increase in capture threshold, either transiently or permanently. This hypothesis was tested in vivo by Dick et al. using an RF ablation catheter at 55 W applied for 60 s on four different pacing and defibrillating leads at different sites, starting 1 cm from the tip of the lead in a tissue bath. Voltage at the tip of the lead was measured during RF energy application, and the leads were then connected to a pacemaker pulse generator to test for a change in function before and after ablation. RF energy delivered less than 1 cm from the electrode tip resulted in a significant current, which may be associated with tissue damage at the cardiac tissue–lead interface. An in vitro study in dogs reported that RF ablation about 1 cm from the tip of the pacing lead resulted in transient oversensing and inhibition of pacing output. Meanwhile, delivering RF lesions 4 cm or more from the lead did not result in lead malfunction.

However, a prospective study showed that atrial ablation can be performed relatively safely in patients with pacemakers and defibrillators (although one patient in the study population had transient increase in atrial lead capture threshold and another had a decrease in atrial sensing after ablation). Therefore, the authors recommend delivering lesions at least 2 cm away from the distal pacing electrode. The same study showed that a higher number of linear lesions was required to achieve success, probably because of the challenge of delivering effective ablation lesions within the close vicinity of a CIED lead. Practically, it is not always possible to stay away from leads while applying RF energy, since critical areas for arrhythmia initiation or maintenance are sometimes located in the close vicinity of a CIED lead. In attempt to have better catheter control while ablating near a CIED lead, the use of a long sheath may be helpful in stabilizing the ablation catheter to avoid contact between the catheter and the lead. Another elegant method is to use a snare to gently remove the lead away from the ablation catheter site. Overall, ablating within 1 cm of the lead tip is not recommended, but it is safe for the lead–tissue interface if the catheter is more than 4 cm away from the tip.

Effects on lead insulation. Society guidelines and CIED manufacturers recommend against using RF energy in close proximity or in direct contact with transvenous leads. Lead insulation defect is the most common reason (56%) for industry-wide ICD lead failure. It has indeed already been demonstrated that RF-based electrocautery, which uses a higher amount of energy/power than catheter ablation, can create insulation damage, especially in polyurethane and copolymer leads (Optim, St. Jude Medical, St. Paul, MN, USA) because of their lower thermal stability. Recently, RF energy application through commonly used ablation catheters was studied in vitro on various commercially-available transvenous CIED leads at maximum power, with irrigated tip catheters, non-irrigated tip catheters, and cryoablation. In this study, the transvenous leads tested included pacemaker, left ventricular and defibrillatory leads of three main commercially used insulation materials (i.e. silicone, polyurethane, and co-polymer). Interestingly, no significant effect was observed on the outer insulation or on lead functionality. This absence of lead damage can be explained by the fact that the temperature achieved with catheter-based RF energy is much lower than that achieved with surgical electrocautery. Generally, RF energy used for cardiac ablation is applied as a continuous, unmodulated sine wave at low voltage, whereas that used for electrocautery is high voltage with a long duty cycle that is designed to promote arcing or coagulum formation. Therefore, the temperature achieved by the RF ablation catheter (up to 106.1°C in the study) is much lower than that achieved by the RF electrocautery cut mode, and is much lower than the melting point of polyurethane (185–225°C) or silicone (has no specific melting point). In addition, the cooling effect of circulating blood flow confers a protective mechanism by helping to reduce the temperature when RF ablation energy is applied on or close to transvenous leads.

Effects on defibrillator coils. RF catheter ablation has been found to be associated with lead malfunction in two studies through a possible effect on defibrillator coils. A study of RF application for AV junction ablation among 59 patients with pre-existing pacemaker or defibrillator implants resulted in a rise in pacing threshold, requiring ventricular lead revision, particularly among the 13 patients with defibrillator leads. This led to lead revision among two out of 13 (15%) patients with defibrillators and two out of 46 (4%) with pacemakers. To date, the mechanism resulting in lead revisions in this study still remains unclear. Hypotheses include the role of the distal ICD coil in conducting some of the dispersed RF energy during ablation, or a possible lead micro-dislodgment, since macrodislodgment was not reported in this study. In a second study, RF has been reported to
result in transient impedance changes in a defibrillator coil, but without longterm sequela.37

**Peri-ablation protocol in patients with cardiac implantable devices**

At our institution, we use the following protocol before starting catheter ablation in a patient with a CIED: (1) turn rate response off (depending on type of rate response and manufacturer); (2) program the device to DOO or VOO mode if the patient is pacemaker-dependent; and (3) disable therapy (i.e. ventricular tachycardia or ventricular fibrillation detection is turned off) in a patient with an ICD. The different steps followed pre-ablation and post-ablation among patients with CIEDs in our institution are presented in **Figure 3**.

**Conclusion**

Various interactions may occur between catheter ablation and CIEDs. It is advised, as a precautionary measure, to program the patient’s CIED prior to ablation to avoid defibrillator therapy and oversensing. In addition, though direct contact of the ablation catheter with the lead has

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**Figure 3:** Proposed algorithm for managing permanent pacemakers and implantable defibrillators before and after a catheter ablation procedure.

* To avoid interference of asynchronous pacing with pacing performed during an EP study.
† Significant changes such as marked increase in capture threshold, profound decrease in sensing or an acute change in impedance measurement.
References

1. Mond HG, Proclemer A. The 11th world survey of cardiac pacing and implantable cardioverter-defibrillators: calendar year 2009—a World Society of Arrhythmia’s project. Pacing Clin Electrophysiol. 2011;34:1013–1027.

2. Zhan C, Baine WB, Sedrakyam A, Steiner C. Cardiac device implantation in the United States from 1997 through 2004: a population-based analysis. J Gen Intern Med. 2007;23(Suppl. 1):13–19.

3. Greenspon AJ, Patel JD, Lau E, Ochoa JA, Frisch DR, Ho RT, et al. Trends in permanent pacemaker implantation in the United States from 1993 to 2009: increasing complexity of patients and procedures. J Am Coll Cardiol. 2012;60(16):1540–5.

4. Cappato R, Calkins H, Chen SA, Davies W, Iesaka Y, Kalman J, et al. Worldwide survey on the methods, efficacy and safety of catheter ablation for human atrial fibrillation. Circulation. 2005;111(9):1100–1105.

5. American Society of Anesthesiologists. Practice advisory for the perioperative management of patients with cardiac implantable electronic devices: pacemakers and implantable cardioverter-defibrillators: an updated report by the American society of anesthesiologists task force on perioperative management of patients with cardiac implantable electronic devices. Anesthesiology. 2011;114(2):247–261.

6. Ellenbogen KA, Wood MA, Stambler BS. Acute effects of radiofrequency ablation of atrial arrhythmias on implanted permanent pacing systems. Pacing Clin Electrophysiol. 1996;19(9):1287–1295.

7. Pfieffer D, Tebbenjohanns J, Schumacher B, Jung W, Lüderitz B. Pacemaker function during radiofrequency ablation. Pacing Clin Electrophysiol. 1995;18(SPt 1):1037–1044.

8. Sadoul N, Blankoff I, de Chillou C, Beurrier D, Messier M, Bizeau O, et al. Effects of radiofrequency catheter ablation on patients with permanent pacemakers. J Intercardiovasc Electrophysiol. 1997;1(3):227–233.

9. Burke MC, Knight BP. Management of implantable pacemakers and defibrillators at the time of noncardiac surgery. ACC Curr J Rev. 2005;14:52–55.

10. Beinart R, Nazarian S. Effects of external electrical and magnetic fields on pacemakers and defibrillators: from engineering principles to clinical practice. Circulation. 2013;128(5):2799–2809.

11. Sweeney MO, Ruetz LL, Belk P, Mullen T, Johnson JW, Sheldon T. Bradycardia pacing-induced short-long-short sequences at the onset of ventricular tachyarrhythmias: a possible mechanism of proarrhythmia? J Am Coll Cardiol. 2007;50(7):614–622.

12. Himrich E, Przibille O, Zellerhoff C, Liebrich A, Rosocha S, Andreas K, et al. Proarrhythmic effect of pacemaker stimulation in patients with implanted cardioverter-defibrillators. Circulation. 2003;108(2):192–197.

13. Siu CW, Tse HF, Lau CP. Avoidance of electromagnetic interference to implantable cardioverter-defibrillator during atrioventricular node ablation for atrial fibrillation using transvenous cryoablation. Pacing Clin Electrophysiol. 2006;29(8):914–916.

14. Jilek C, Tzeis S, Reents T, Estner HL, Fichtner S, Ammar S, et al. Safety of implantable pacemakers and cardioverter defibrillators in the magnetic field of a novel remote magnetic navigation system. J Cardiovasc Electrophysiol. 2010;21(10):1136–1141.

15. Lüthje L, Vollmann D, Seegers J, Sohns C, Hasenfuss G, Zabel M. Interference of remote magnetic catheter navigation and ablation with implanted devices for pacing and defibrillation. Europace. 2010;12(11):1574–80.

16. Jilek C, Lennerz C, Stracke B, Badran H, Stemmler V, Reents, et al. Forces on cardiac implantable electronic devices during remote magnetic navigation. Clin Res Cardiol. 2013;102(3):185–192.

17. Eitel C, Hindricks G, Sommer P, Wetzel U, Bollmann A, Gaspar T, et al. Safety of remote magnetic navigation in patients with pacemakers and implanted cardioverter defibrillators. J Cardiovasc Electrophysiol. 2010;21(10):1130–1135.

18. Friedman DJ, Parzynsky CS, Varosy PD, Prutkin JM, Patton KK, Mithani A, et al. Trends and in-hospital outcomes associated with adoption of the subcutaneous implantable cardioverter defibrillator in the United States. JAMA Cardiol. 2016;1(8):900–911.

19. Martínez-Sande JL, García-Seara J, Rodríguez-Mañero M, Fernández-López XA, González-Melchor L, Redondo-Díezgua A, et al. The Micra leadless transcatheter pacemaker. Implantation and mid-term follow-up results in a single center. Rev Esp Cardiol (Engl Ed). 2016. [Epub ahead of print].

20. Lakikreddy D, Patel D, Ryschon K, Bhateja R, Bhakru M, Thal S, et al. Safety and efficacy of radiofrequency energy catheter ablation of atrial fibrillation in patients with pacemakers and implantable cardiac defibrillators. Heart Rhythm. 2005;2(12):1309–16.

21. Reddy VY, Morales G, Ahmed H, Neuzil P, Dukkipati S, et al. Catheter ablation of atrial fibrillation without the use of fluoroscopy. Heart Rhythm. 2010;7(11):1644–1653.

22. Chang AC, McCarevey D, Tripodi D, Fanaanazpir L. Radiofrequency catheter atrioventricular node ablation in patients with permanent cardiac pacing systems. PACE. 1994;17:65–69.

23. Kilborn MJ, McGuire MA. Radiofrequency catheter ablation of atrioventricular junctional (‘‘AV nodal’’) reentrant tachycardia in patients with implantable cardioverter defibrillators. Pacing Clin Electrophysiol. 1998;21(12):2681–2684.

24. Proclemer A, Facchin D, Pagnutti C, Fioretti P, De Michele C. Safety of pacemaker implantation prior to radiofrequency ablation of atrioventricular junction in a single session procedure. Pacing Clin Electrophysiol. 2000;23(6):998–1002.

25. Furman S, Pannizzo F, Campo I. Comparison of active and passive adhering leads for endocardial pacing. Pacing Clin Electrophysiol. 1997;20(2):417–427.

26. Bardy GH, Hofer B, Johnson G, Kudenchuk PJ, Poole JE, Dolack GL, et al. Implantable transvenous cardioverter-defibrillators. Circulation. 1993;87(4):1152–1168.

27. Crossley GH, Poole JE, Rozner MA, Asirvatham SJ, Cheng A, Chung MK, et al. The Heart Rhythm Society (HRS)/American Society of Anesthesiologists (ASA) Expert Consensus Statement on the perioperative management of patients with implantable defibrillators, pacemakers and arrhythmia monitors: facilities and patient management this document was developed as a joint project with the American Society of Anesthesiologists (ASA), and in collaboration with the American Heart Association (AHA), and the Society of Thoracic Surgeons (STS). Heart Rhythm. 2011;8(7):1114–1154.

28. Dick AJ, Jones DL, Klein GJ. Poster abstracts: Effects of RF energy delivery to pacing and defibrillation leads. PACE. 2001;24(4P2):658.
29. Chin MC, Rosenqvist M, Lee MA, Griffin JC, Langberg JJ. The effect of radiofrequency catheter ablation on permanent pacemakers: An experimental study. *PACE*. 1990;13(1):23–29.

30. Newby KH, Zimerman L, Wharton JM, Ken V, Kearney M, Brandon MJ, Natale A. Radiofrequency ablation of atrial flutter and atrial tachycardias in patients with permanent indwelling catheters. *Pacing Clin Electrophysiol.* 1996;19(11):1612–1617.

31. Darrat YH, Morales GX, Waespe C, Gurley JC, Elayi CS. Snaring of the right ventricular lead during cavotricuspid isthmus ablation. *Clin Case Rep.* 2017;5(3):312–314.

32. Kleemann T, Becker T, Doenges K, Vater M, Senges J, Schneider S, et al. Annual rate of transvenous defibrillation lead defects in implantable cardioverter-defibrillator over a period of >10 years. *Circulation.* 2007;115(19):2474–2480.

33. Lim KK, Reddy S, Desai S, Smelley M, Kim SS, Beshai JF, et al. Effects of electrocautery on transvenous lead insulation materials. *J Cardiovasc Electrophysiol.* 2009;20(4):429–435.

34. Darrat YH, Agarwal A, Morales GX, Thompson J, Abdel-Latif A, Waespe K, et al. Radiofrequency and cryo-ablation effect on transvenous pacing and defibrillatory lead integrity: An *in vitro* study. *J Cardiovasc Electrophysiol.* 2016;27(8):976–980.

35. Kalbfleisch SJ, Langberg JJ. Catheter ablation with radiofrequency energy: biophysical aspects and clinical applications. *J Cardiovasc Electrophysiol.* 1992;3:173–186.

36. Burke MC, Kopp DE, Alberts M, Patel A, Lin AC, Kall JG, et al. Effect of radiofrequency current on previously implanted pacemaker and defibrillator ventricular lead systems. *J Electrocardiol.* 2001;34 Suppl:143–148.

37. Vanga SR, Bommana S, Kroll M, Lakkireddy D. Impedance changes on defibrillation coils after atrial fibrillation ablation: lead damage or electromechanical interference? *Pacing Clin Electrophysiol.* 2012;35(6):e163–166.