Fractional flow reserve (FFR) is conducted to evaluate the need for percutaneous coronary intervention (PCI) for moderate stenosis of the coronary artery. FFR is calculated by measuring the pressure within the coronary artery proximal and distal to the coronary artery stenotic lesion. For example, an FFR of 0.50 means that the actual blood flow is only 50% of the maximum blood flow you would normally see because of the stenosis. Normally, PCI is used when FFR is >0.80. 1–3

Computational Fluid Dynamics (CFD) is the study of understanding the mechanism of the “flow” created when the fluid represented by air and water moves, taking a physical and engineering approach. 4–6 CFD is a simulation method used to compute approximate solutions by discretizing the Navier-Stokes equation, an equation that describes the movement of viscous fluids and is used to understand hemodynamics. The advantages of using CFD are that large-scale research facilities are not needed and there is no cost associated with repeating analyses multiple times. Conversely, a disadvantage of CFD is that errors may be introduced as a result of the various hypotheses and models used in the equation. Because of the evolution in computational ability, CFD analyses can now be performed using general-purpose computers and CFD software. Recently, blood flow simulations have been adopted in the medical field. 7 In the congenital heart disease field, because morphology is anatomically complex and there are dynamic changes in blood flow after surgery, CFD has been used to predict hemodynamics since 1995, contributing to the determination of surgical indications and understanding postoperative hemodynamics. 8, 9 Moreover, most vascular diseases, such as thrombosis, arteriosclerosis, and formation of aneurysms, of the human circulatory system occur at junctions and in curved sections of relatively large vessels, as well as in the lower reaches of constricted parts. Clinical studies and autopsies have demonstrated that formation of aneurysms appear locally at sites where the blood flow is disturbed in a hydrodynamic view, suggesting that there is a relationship between blood flow and the onset of vascular diseases. 10 Many studies have also been conducted in the cerebrovascular field using CFD, including the prediction of which aneurysm will rupture among unruptured cerebral aneurysms found occasionally, 11 analysis of the flow within the aortic arch, which has various
kinks, and the study of fluid dynamics with regard to the form of arcs and the onset of aneurysms.12–16
In the present study, we revealed the relationship between FFR, which is determined during intracardiac catheterization for moderate stenosis of the coronary artery, and CFD analysis using cardiac computed tomography (CT), and then examined whether CFD can be used to evaluate ischemia.

Methods

Materials
Angiograms were performed using a PHILIPS Allura Xper FD 10/10, CT was performed using a SIEMENS SOMATOM Force CT scanner, 3-dimensional (3D) analysis was performed using an AMIN ZIO Station 2 workstation, and CFD analysis was performed using Hemoscope 2015 software. A stenosis phantom was used in the phantom experiment.

Patients
Information was collected retrospectively for patients with coronary CT-identified moderate stenosis in the coronary arteries and in whom FFR was measured by cardiac catheterization within 3 months between January 2013 and March 2020 (Table).

Basic Examination Using a Stenosis Phantom
CFD analysis was conducted for constricted parts using a stenosis phantom with known stenosis rates. The blood vessel diameter of the stenosis phantom was 5.00 mm and

| Table. Patient Characteristics |
|-----------------------------|
| Sex (n)                     |
| Male                        | 167 |
| Female                      | 62  |
| Age (years)                 | 72±11 |
| Location of stenotic lesion (n) |
| RCA                        | 52  |
| LAD                        | 134 |
| LCx                        | 43  |
| QCA                         |
| % Stenosis                  | 51.7±18.7 |
| MLD (mm)                    | 2.3±0.7  |
| Plaque volume (mm³)         | 29.9±11.8 |
| MLA (mm²)                   | 3.1±0.39 |
| No coronary risk factors    | 24 (10.5) |
| Hypertension                | 163 (71.2) |
| Diabetes                    | 93 (40.6) |
| Hyperlipidemia              | 22 (9.6) |
| Dyslipidemia                | 102 (44.5) |
| Smoking (including past smoker) | 70 (30.6) |
| Hyperuricemia               | 34 (14.8) |
| Old myocardial infarction   | 84 (36.7) |
| Chronic renal failure       | 48 (21.0) |
| Family history of coronary event | 29 (12.7) |

Unless indicated otherwise, data are given as the mean±SD or as n (%). LAD, left anterior descending artery; LCX, left circumflex artery; RCA, right coronary artery; MLA, minimum lumen area; MLD, minimal lumen diameter; QCA, quantitative coronary angiography.

Figure 1. Results of the computational fluid dynamics (CFD) analysis of wall pressure (WP) and wall shear stress (WSS) using a stenosis phantom.
the stenosis rates were 50% and 75%. Contrast medium was loaded inside the stenosis phantom and images were obtained using CT. The CT images obtained were then used to create volume rendering images. CFD analysis was conducted on the volume rendering images and the behavior of wall pressure (WP) and wall shear stress (WSS) on the stenotic lesion were confirmed. The WP and WSS thresholds were fixed. Blood flow simulation was conducted using a CT image (512×512 pixels, slice thickness 0.75 mm, slice interval 0.6 mm). CFD analysis software hemoscope 2015 was used to extract blood vessels. The half-value method was used to evaluate blood vessels. Blood was defined as an incompressible Newtonian fluid with a density (ρ) of 1,050 kg/m³ and viscosity (μ) of 0.004 Pa·s. A steady flow was used for the analysis. The finite volume method was used for analysis of the flow equation. A 3D unsteady calculation method was used. The computational mesh of the major area consisted of a tetra mesh with a model length of 0.2 mm. The mesh of the boundary layer area was a prism mesh of the wall-nearest grid (height 0.05 mm, width 0.2 mm). The time acceleration item of the Navier-Stokes equation was calculated using the Euler equation, whereas the space acceleration item was a second-order upwind differencing scheme.

**Relationship Between FFR and CFD Analysis**

The WP and WSS of CFD analyses calculated using FFR were compared with the results of coronary CT in patients

---

**Figure 2.** Correlation between fractional flow reserve (FFR) and (A) wall pressure (WP) and (B) wall shear stress (WSS), determined by computational fluid dynamics analysis, in the right coronary artery.

**Figure 3.** Correlation between fractional flow reserve (FFR) and (A) wall pressure (WP) and (B) wall shear stress (WSS), determined by computational fluid dynamics analysis, in the left anterior descending artery.
Received Operating Characteristic Analysis of WSS
Cardiac catheterization yielded 120 lesions with FFR < 0.08 deemed positive and 109 lesions with FFR ≥ 0.80 deemed negative. Receiver operating characteristic (ROC) analysis was performed on each coronary artery to determine the WSS cut-off value.

Statistical Analysis
The significance of differences in WSS between patients in whom PCI was performed and those in whom it was deferred was determined using a Wilcoxon rank-sum test. ROC analysis was used to define cut-off values by minimizing the expression $(1 - \text{sensitivity})^2 + (1 - \text{specificity})^2$. Statistical analyses were performed using JMP pro 14. Two-sided $P < 0.05$ was considered significant.

Ethical Considerations
This study was approved by the Ethics Committee of Showa University, Japan. The study was conducted in accordance with the ethical principles based on the Declaration of Helsinki and the ethical guidelines for human medical research, and complied with this study implementation plan.

Results

Basic Examination Using a Stenosis Phantom
CFD analysis using a stenosis phantom revealed increasing WP on the proximal side of the constriction site as the stenosis rate of the stenosis phantom increased, and decreasing WP on the distal side. The WSS at the constriction site was also increased with an increasing stenosis rate of the stenosis phantom (Figure 1).

Relationship Between FFR and CFD Analysis
No correlation was seen between WP determined by CFD analysis and FFR for each segment of the RCA in 52 patients with ischemic heart disease, with a correlation coefficient ($r$) of 0.23 (Figure 2A). There was a tendency for WP to be higher on the proximal side of the lesion as the
was a correlation between WSS determined by CFD analysis in each segment of the LCx and FFR (r=0.69; Figure 4B). Setting a cut-off value for FFR of 0.80, WSS was significantly higher in the group of patients in whom PCI was performed than in those in whom the procedure was deferred (Figure 5).

ROC Analysis of WSS
Using ROC analysis of cut-off values of WSS at an FFR of <0.08 revealed that the sensitivity and specificity of a WSS cut-off value of 598 kPa (5.9 atm) were 100% and 97.2%, respectively, in the RCA (Figure 6A) and 81.9% and 94.1%, respectively, in the LAD (Figure 6B). At a cut-off value of 588 kPa (5.8 atm) for WSS in the LCx, sensitivity degree of stenosis. Conversely, the WSS of CFD analysis in each segment of the RCA was correlated with FFR (r=0.81; Figure 2B).

Similarly, for each segment of the LAD in 134 patients with ischemic heart disease, there was no correlation between WP determined by CFD analysis and FFR (r=0.006; Figure 3A). There was a tendency for WP to be higher on the proximal side as the rate of stenosis increased, similar to findings in the RCA. Conversely, there was a correlation for WSS determined by CFD analysis in each segment of the LAD and FFR (r=0.71; Figure 3B).

WP determined by CFD analysis in each segment of the LCx in 43 patients with ischemic heart disease was not correlated with FFR (r=0.07; Figure 4A). Conversely, there was a correlation between WSS determined by CFD analysis in each segment of the LCx and FFR (r=0.69; Figure 4B). Setting a cut-off value for FFR of 0.80, WSS was significantly higher in the group of patients in whom PCI was performed than in those in whom the procedure was deferred (Figure 5).

**ROC Analysis of WSS**
Using ROC analysis of cut-off values of WSS at an FFR of <0.08 revealed that the sensitivity and specificity of a WSS cut-off value of 598 kPa (5.9 atm) were 100% and 97.2%, respectively, in the RCA (Figure 6A) and 81.9% and 94.1%, respectively, in the LAD (Figure 6B). At a cut-off value of 588 kPa (5.8 atm) for WSS in the LCx, sensitivity
and specificity were 71.4% and 100%, respectively (Figure 6C).

**Discussion**

**Basic Examination Using a Stenosis Phantom**

In the basic examination using a stenosis phantom, WP was high on the proximal side of the stenosis phantom and low on the distal side. Based on Bernoulli’s law, because fluid flow velocity is faster at constricted parts than in parts with no stenosis, the WP at the site of constriction decreased when fluid flowed through the constricted part. The stenosis phantom used for the basic examination in this study demonstrated that WP was low after passing through the constricted part. The cause of this is considered to be energy loss due to the detachment of flow after constriction. Conversely, WSS at the constricted part increased as the stenosis rate of the stenosis phantom increased. It was assumed that the values of WSS was high because of the emergence of a vortex at the constricted part.

**Relationship Between FFR and CFD Analysis**

CFD analysis using clinical cases with focal stenosis showed that WP increased on the proximal side of the stenosis (Figure 7A). The greater the degree of stenosis, the greater the pressure loss after the stenosis. Therefore, if WP after the stenosis is low, it is considered that ischemia is present distal to the stenosis. However, WP was not correlated with FFR in each coronary artery. This is probably because the degree of pressure loss varies depending on the location of the stenosis.

Conversely, in clinical cases, WSS increased in the stenosis, which was considered to be due to turbulent flow in the stenosis, as in the basic examination in the stenosis phantom (Figure 7B). WSS was correlated with FFR because the WSS at the stenosis increases as the stenosis increases. Moreover, using a cut-off value of 0.80 for FFR revealed that WSS was significantly higher in patients who underwent PCI than in those in whom PCI was deferred. This can be explained by sections with both high and low forces rubbing against the vascular wall because of biologic factors, pathologic stenosis, junctions, etc. in the blood vessels, in addition to the occurrence of a vortex and turbulent flow at the site of constriction.

Reynolds number (Re) is used to determine whether flow is likely to be laminar or turbulent. The Re of coronary flow is 800<Re<1,000. Generally, Re is used as an indicator to indicate the transition from laminar to turbulent flow, with flow becoming turbulent when Re is >2,300. The velocity of fluid flow is faster when the stenosis is larger. We believe that because Re increases if viscosity is low and velocity of fluid flow is faster when the stenosis is larger, with flow becoming turbulent when Re is >2,300.

**ROC Analysis of WSS**

Using cut-off values of WSS of 598 kPa (5.9 atm) in the RCA and LAD and 588 kPa (5.8 atm) in the LCx at an FFR of <0.08, resulted in sensitivity and specificity of 100% and 97.2%, respectively, in the RCA, 81.9% and 94.1%, respectively, in the LAD, and 71.4% and 100%, respectively, in the LCx. Using the stenosis phantom, the cut-off value of WSS when the stenosis rate was 75%, which is considered a significant stenosis in coronary arteries, was 608 kPa (6.0 atm). The cut-off values for WSS calculated by ROC analysis in clinical cases were 598 kPa (5.9 atm) for the RCA and LAD and 588 kPa (5.8 atm) for the LCx, which are equivalent to the value determined in the phantom experiment. Therefore, the WSS cut-off value for each coronary is considered to have high validity. Thus, evaluating ischemia by calculating the WSS using CFD analysis for moderate stenosis of the coronary artery is considered possible.

We believe that a comparison of the diagnostic accuracy following evaluation of FFR in CT angiography is necessary. Driessen et al reported a diagnostic accuracy, sensitivity, and specificity of 87%, 90%, and 86%, respectively, for FFRCT<0.80 identifying stenosis >90%. Conversely, Nakazato et al reported a diagnostic accuracy, sensitivity, and specificity of 71%, 74%, and 67%, respectively, for lesions of intermediate stenosis severity. CFD analysis using FFR with a WSS cut-off value <0.80 has a higher per-vessel sensitivity and specificity, and can be considered a useful technique.

The present study has some limitations. First, CFD analysis is significantly affected by the images used in the analysis. It is unclear to what degree blood vessel diameter and CT value of the 3D construction image affected the results of the CFD analysis in this study.

**Conclusions**

We revealed the relationship between FFR, which is calculated during intracardiac catheter testing for moderate stenosis of the coronary artery, and CFD analysis using cardiac CT images. The findings suggest that evaluating ischemia of coronary arteries is possible by calculating the WSS using CFD analysis of cardiac CT images.

**Sources of Funding**

This study did not receive any specific funding.

**Disclosures**

There is no conflict of interest to disclose.

**IRB Information**

This study was approved by the Ethics Committee of Showa University, Japan (Reference no. 2783).

**References**

1. Bech GJ, De Bruyne B, Pijls NH, de Muinck ED, Hoornije JC, Escaned J, et al. Fractional flow reserve to determine the appropriateness of angioplasty in moderate coronary stenosis: A randomized trial. Circulation 2001; 103: 2928–2934.
2. Pijls NHJ, van Schaardenburgh P, Manoharan G, Boersma E, Bech JW, van’t Veer M, et al. Percutaneous coronary intervention of functional nonsignificant stenosis: 5 year follow up of the DEFER study. Am J Cardiol 2007; 49: 2105 – 2111.
3. De Bruyne B, Fearon WF, Pijls NHJ, Barbato E, Tonino P, Piroth Z, et al. Fractional flow reserve-guided PCI for stable coronary artery disease. N Engl J Med 2014; 371: 1208–1217.
4. Libby P, Okamoto Y, Rocha VZ, Folco E. Inflammation in atherosclerosis: Transition from theory to practice. Circ J 2010; 74: 213–220.
5. Chatzizisis YS, Jonas M, Coskun AU, Beigel R, Stone BV, Maynard C, et al. Prediction of the localization of high-risk coronary atherosclerotic plaques on the basis of low endothelial shear stress: An intravascular ultrasound and histopathology natural history study. Circulation 2008; 117: 993–1002.
6. Hwang J, Saha A, Boo YC, Soreseu GP, McNally JS, Holland...
SM, et al. Oscillatory shear stress stimulates endothelial production of O2 from p47phox-dependent NAD(P)H oxidases, leading to monocyte adhesion. J Biol Chem 2003; 278: 47291 – 47298.

7. Takao H, Yamamoto M, Otsuka S, Suzuki T, Masuda S, Murayama Y, et al. Analysis of cerebral aneurysms using computational fluid dynamics (CFD). Jpn J Neurosurg 2012; 21: 298 – 305.

8. Itatani K, Miyaji K, Tomoyasu T, Nakahata Y, Ohara K, Takamoto S, et al. Optimal conduit size of the extracardiac Fontan operation based on energy loss and flow stagnation. Ann Thorac Surg 2009; 88: 565 – 573.

9. Itatani K, Miyaji K, Nakahata Y, Ohara K, Takamoto S, Ishii M. The lower limit of the pulmonary artery index for the extracardiac Fontan circulation. J Thorac Cardiovasc Surg 2011; 142: 127 – 135.

10. Wada S, Nokari T, Naiki T. Effects of physical and hydrodynamic factors on the localization of vascular disease. Electronic Sci Res 1997; 4: 22 – 32.

11. Yagi T, Qian Y, Takao H, Murayama Y, Umez U. Toward establishing medical engineering technology to predict rupture of cerebral aneurysm. Artif Organs 2010; 39: 227 – 231.

12. Mori D, Yamaguchi T. Computational hydrodynamic analysis of the effect of intra-aortic blood flow in the development of aortic aneurysm. Jpn Coll Angiol 2003; 43: 94 – 97.

13. Fung YC. Biomechanics: circulation. New York: Springer Verlag, 1997; 58 – 69.

14. White FM. Viscous fluid flow. McGraw-Hill, 2005; 1259 – 1269.

15. Takao H, Murayama Y, Otsuka S, Qian Y, Mohamed A, Masuda S, et al. Hemodynamic differences between unruptured and ruptured intracranial aneurysms during observation. Stroke 2012; 43: 1436 – 1439.

16. Miura Y, Ishida F, Umeda Y, Tanemura H, Suzuki H, Matsushima S, et al. Low wall shear stress is independently associated with the rupture status of middle cerebral artery aneurysms. Stroke 2013; 44: 519 – 521.

17. Takagi S, Matsumoto Y. Multiphase flows in bio-medical field. Jpn J Multiphase Flow 2012; 26: 386 – 391.

18. Driessen RD, Danad I, Stuijfzand WJ, Raijmakers PG, Schumacher SP, van Diemen PA, et al. Comparison of coronary computed tomography angiography, fractional flow reserve, and perfusion imaging for ischemia diagnosis. J Am Coll Cardiol 2013; 6: 881 – 889.