A thermo-physical analysis of the proton pump vacuolar-ATPase: the constructal approach

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Pumping protons across a membrane was a critical step at the origin of life on earth, and it is still performed in all living organisms, including in human cells. Proton pumping is paramount to keep normal cells alive, e.g. for lysosomal digestion and for preparing peptides for immune recognition, but it goes awry in cancer cells. They acidify their microenvironment hence membrane voltage is lowered, which in turn induces cell proliferation, a hallmark of cancer. Proton pumping is achieved by means of rotary motors, namely vacuolar ATPases (V-ATPase), which are present at many of the multiple cellular interfaces. Therefore, we undertook an examination of the thermodynamic properties of V-ATPases. The principal result is that the V-ATPase-mediated control of the cell membrane potential and the related and consequent environmental pH can potentially represent a valuable support strategy for anticancer therapies. A constructal theory approach is used as a new viewpoint to study how V-ATPase can be modulated for therapeutic purposes. In particular, V-ATPase can be regulated by using external fields, such as electromagnetic fields, and a theoretical approach has been introduced to quantify the appropriate field strength and frequency for this new adjuvant therapeutic strategy.

A fundamental characteristic of intracellular membrane compartments is the difference between their luminal pH and the bulk cytoplasm pH. The vacuolar ATPase is the main mechanism responsible for this pH differential¹. These proteins include a class of proton pumps structurally homologous to the F-ATPases that produce ATP by using the proton-motive force across the mitochondrial inner membrane²-⁴. A vast amount of new information has been obtained on the structure, mechanics, and biochemistry of the F-ATPases. For example, the rotation of the F₁ motor was proven to develop over 40 pN nm and advance in three steps per revolution, with the hydrolysis of one ATP for each step⁵. Moreover, the F₀ motor was found to consist of 10 or 12 subunits with rotational symmetry⁶. The F₀ motor counters the large F₁ torque by generating an even larger torque in the opposite direction to synthesize ATP. To do so it converts the transmembrane proton-motive force into rotary motion.

A mechanochemical model for the V-ATPase was suggested by Grabe, Wang, and Oster². This model allows us to predict proton pumping rates over a wide range of environmental conditions which proves useful to determine the acidification of organelles. The model is based on the hypothesis that the V-ATPase works under normal operating conditions and that ATP concentrations are sufficiently high so that hydrolysis is not rate limiting⁷. The V-ATPase structure is composed of a counter-rotating stator and a rotor. The membrane-inserted/transmembrane section V₀ is affected by the hydrolysis of ATP in the V₁-soluble headpiece. A two-channel model and a one-channel model have been suggested to explain the rotor-stator assemblies⁸. They differ in the protons’ path through the enzyme and communicate with the cytoplasm through the protons bound to the rotor section⁹. However, some experiments on sodium V-ATPases seem to support the one channel model⁸.

The accepted model for the active transmembrane ion transport is the alternating access mechanism. Ions are bound tightly on the low concentration side of the membrane. A conformational change weakens their binding affinity by exposing them to the high concentration side; as a consequence, they dissociate. Then, the pump changes its conformation in order to begin the cycle again⁸.

These types of processes are usually described by mechanochemical approaches. But, recently, an applied thermodynamic approach has been developed to analyse the biophysical and biochemical behaviour of the
Cells are composed of a cyclic process. Indeed, it begins with the emergence from cell phenomenon occurring within a particular range. So a cell’s life is the size of any cell can vary as well as their daughters’ sizes, a each of them divides into two different daughter cells. At that time, and, at a proper time and depending on the tissues they belong to, physical and biochemical mechanisms inside the cell12. But this kind of analysis is powerfully described by the constructal theory. Indeed, by referring to the constructal law, a living system presents two characteristics: its flows and it morphs freely toward configurations that allow all its currents to flow more easily over time12. Life and evolution are a physics phenomenon, and they belong in physics86. Constructal law is a new approach introduced in thermodynamics in order to explain optimal shapes of natural structures13,14,15,16,19,20. The fundamental bases of the Constructal law was expressed2 as follows: “For a finite-size flow system to persist in time (to live), its configuration must evolve in such a way that provides greater and greater access to the currents that flow through it.”

But, in a cell, a part of the energy is lost as heat outflow and only the resulting products of biochemical processes are known, while any individual step is inaccessible27. So, a constructal approach can represent a powerful theoretical method to analyse cell behaviour. Indeed, constructal theory highlights the fundamental role that flows across the system’s border play in any thermodynamic process. This can represent a new viewpoint in the analysis of the biochemical and biophysical behaviour of cells. Instead of studying the cell, a very complex system, we can now study how the cells exchange components and information with their environments, and the interactions between cells and environments, which consist of the flows across the cell membranes. Indeed, cells are so complex that it is very difficult to understand the single effect of a given cellular process in relation to the ‘global’ result for the cell. Consequently, the study of cells can be developed by introducing the black box model, and considering only the spontaneous cell flows. Therefore the spontaneous heat cell exchange represents the interaction or, here, spontaneous communication between the cell and its environment. Lastly, it is, of course, easier to access the environment than the living cell.

Therefore, we decided to analyse the heat and mass flows across the membrane. This is what following a constructal approach suggests. But, in the analysis of the cell membrane, in relation to the molecular motors involved in this process, we have no useful data to evaluate directly the flows. Consequently we use constructal theory as a new fundamental viewpoint but we need a related method to develop the calculations. Notably, the heat flow is the consequence of the irreversible processes within cells and this is easily developed by using the Gouy-Stodola theorem22; it considers only the work lost for irreversibility and the temperature of the system’s environment. This constructal based approach is theoretically interesting because25:

- It allows to obtain the physical conditions in which an open system persists in its stationary states;
- This is a power description of complex phenomena because it allows to evaluate the global effects and their fluctuations around the stationary states;
- It involves the definition of exergy flows, which are the flows of the available energy of the system.

In 1873, Gibbs introduced the available energy, today named exergy. It is the function that expresses the maximum useful work that a system can obtain in a thermodynamic equilibrium with its environment. The exergy lost or dissipated $E_i$, i.e. the available energy or work lost $W_i$, in an irreversible process, for us the heat emerging from the cell, can be obtained through the Gouy-Stodola theorem25:

$$E_i = W_i = T_0 S_q$$

(1)

with $T_0$ the environment temperature and $S_q$ the entropy generation. By using this relation and evaluating any process across the membrane, always by using the well accepted applied thermodynamic relations21, the exergy flows across the membrane can be related to the entropy generation for a cell which has recently obtained28–32 as:

The approach to irreversibility. Cells are living systems. They grow and, at a proper time and depending on the tissues they belong to, each of them divides into two different daughter cells. At that time, the size of any cell can vary as well as their daughters’ sizes, a phenomenon occurring within a particular range. So a cell’s life is a cyclic process. Indeed, it begins with the emergence from cell separation, and it ends with the separation of the daughter cells. Cells are composed of:

- The cellular membrane, which controls the mass and energy inflow and outflow;
- The cytoplasm, an aqueous solution containing thousands of structures and a vast array of chemical species;
- The organelles, specialised subunits suspended in the cytoplasm, each enclosed within a membrane separating it from the cytoplasm. They perform specific, specialized, functions;
- A network of tubular structures maintaining cell form, and allowing directional transport such as microtubules, cilia, organizer.

Within cells, chemical reactions occur that produce energy and macromolecules, and that increase and modify cell volume and its form17.

From a thermodynamic point of view, cells are open and complex systems able to convert their energy in the most efficient way for transport of substances across their membranes. They behave in two distinctively different ways: evolving towards maximum disorder or maintaining a high degree of organization in space and time. To do so, they must couple metabolic and chemical reactions with transport processes across their borders18.

Any system in nature has shape and structure25. They are macroscopic, finite size, and recognizable as patterns. The previous classical thermodynamic analysis highlighted that the flows in cell systems are fundamental to evaluate the behaviour of the systems themselves. Consequently, the analysis of the flows through the cell membrane appears fundamental in the comprehension of the biophysical and biochemical mechanisms inside the cell17. But this kind of analysis is powerfully described by the constructal theory. Indeed, by referring to the constructal law, a living system presents two characteristics: its flows and it morphs freely toward configurations that allow all its currents to flow more easily over time12. Life and evolution are a physics phenomenon, and they belong in physics86. Constructal law is a new approach introduced in thermodynamics in order to explain optimal shapes of natural structures13,14,15,16,19,20. The fundamental bases of the Constructal law was expressed2 as follows: “For a finite-size flow system to persist in time (to live), its configuration must evolve in such a way that provides greater and greater access to the currents that flow through it.”

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\[ S_g = S_{g,th} + S_{g,d} + S_{g,cc} + S_{g,c} + S_{g,ad} = \]
\[ = \frac{\mu L^2 \bar{x}_{th}}{6T^2} \Delta T \tau_1 + \frac{\bar{x}_{th} V^2}{T} \sum i \mu_i (\mu_{i,ar} - \mu_{i,ir}) \frac{d_m}{\tau_2} \]
\[ + \frac{4\pi}{T} \frac{\bar{x}_c^2}{r_{de}} + V \tau_4 \sum_i N_i \bar{A}_i \int dV \int \frac{dV'}{T} \sum_k \Pi_k F_k \]

where:

1. \( S_{g,th} \) is the entropy generation due to the thermal flux driven by the temperature difference, in which \( \tau_1 \) is the lifetime of this process;
2. \( T \) is the temperature;
3. \( S_{g,d} \) is the entropy generation due to the diffusion current driven by the chemical potential gradients, in which \( \tau_2 \) is the lifetime of this process, \( \mu_i \) is the chemical potential of the \( i \)-th species;
4. \( S_{g,v} \) is the entropy generation due to the velocity gradient coupled with the viscous stress, in which \( \tau_3 \) is the lifetime of this process;
5. \( S_{g,cc} \) is the entropy generation due to the chemical reaction rate driven by the affinity, in which \( \tau_4 \) is the lifetime of this process, \( N_i \) is the number per unit time and volume of the \( i \)-th chemical reaction and \( \beta \) is the affinity, evaluated as the variation of the standard Gibbs’ free energy;
6. \( S_{g,c} \) is the entropy generation due to the dissipation that results from the interaction between external forces and the system, in which \( \tau_5 \) is the lifetime of this process, \( F \) is the force generated by the interaction with the external field and \( J \) is the associated flow.
7. Where the volume of the cell is defined as \( V \)
\[ V = \frac{\delta_1(t) \delta_2(t)}{2} \]  
with \( \delta_1(t) \) and \( \delta_2(t) \) the long and the short axes dimensions of the cell, but \( \delta_1(t) \) and \( \delta_2(t) \) must be experimentally evaluated, so for a theoretical approach the diameter of the cell is approximated as the diameter of a sphere:
\[ L = \left( \frac{6V}{\pi} \right)^{1/3} \]  
Consequently, the characteristic length of the cell results in:
\[ L = \left( \frac{3 \delta_1(t) \delta_2(t)}{\pi} \right)^{1/3} \]  
8. \( r = L/2 \) is the cell radius
9. The mean environmental temperature can be assumed to be \( T_0 = 310 \text{ K} \) and the mean cell temperature has been estimated to be \( T_0 + \Delta T \);
10. \( \Delta T \) is the difference between the temperature inside the cell and that of its environment. It has been evaluated as \( \Delta T = 0.4 \text{ C} \), but it would be different for each cell line and for each cell line it would have to be different between normal and cancerous (or more generally, diseased) states;[11]
11. The characteristic length \( L \) can be evaluated as \( L = 2 \, r \);
12. The internal energy density \( u \) can be evaluated as the ratio between the cell’s mean internal energy, considered the same as that of ATP, \( U = 3 \times 10^{-7} \text{ J} \) and the mean value of the cell inside the human body \( V = 7600 \mu \text{m}^3 \), hence the cell volume in the human body being in the range 200–15000 \mu m^3, so it results in \( u = 3.95 \times 10^7 \text{ J m}^{-3} \);
13. The thermal molecular mean velocity inside the cytoplasm is considered to be \( \bar{x}_{th} = 5 \times 10^{-4} \text{ m s}^{-1} \);
14. \( \bar{v} \) can be assessed as \( \bar{v} = 0.2 \, r \).
15. The membrane volume is evaluated as \( V_m = 4 \frac{\pi}{3} r^3 = 4 \frac{\pi}{3} (r - d_c)^3 = 0.992V \)

with \( \pi = 3.14 \);
16. The chemical potential gradient \( \mu \) can be calculated as the ratio between the mean value of the chemical potential \( \mu = 1.20 	imes 10^{-3} \text{ J kg}^{-1} \) and the membrane length \( d_m = 0.01 \mu \text{m} \), with the mean density being \( \rho = 1000 \text{ kg m}^{-3} \);
17. The viscosity \( \eta \) is taken to be \( 6.91 \times 10^{-3} \text{ N s m}^{-2} \);
18. \( \eta \sim 2.07 \times 10^{-3} \text{ N s m}^{-2} \) at \( \text{pH} \);[12, 17] 30 °C.
19. \( \bar{x}_n \) is evaluated as \( \bar{x}_{th} = 3.0 \times 10^{-4} \text{ m s}^{-1} \);
20. \( F_k \) is the external field and \( J_k \) is the associated flow.

**Constructal approach to V-ATPase.** The basis of metabolism energetics consists in the generation and the hydrolysis of ATP, which occurs across a trans-membrane electromotive gradient. Indeed, this conversion of energy can be obtained by transitioning the electrochemical energy into the chemical energy of the terminal phosphoric anhydride bond of the ATP(5). This can occur by the action of an enzyme, which works as a proton-pumping ATP synthetase. Here the proton pump V-ATPase will be discussed by introducing just the constructal approach.

As described in the introduction, the V-APTase works through a counter-rotating stator and a rotor mechanism. It hydrolyses ATP to obtain the required energy for its work. The fundamental reaction is:
\[ \text{ATP} + \text{H}_2\text{O} \rightarrow \text{ADP} + \text{P} \]
and, consequently, a H⁺ ion is pumped into the cell:
\[ \text{H}^+_{\text{out}} \rightarrow \text{H}^+_{\text{in}} \]
where out means outside, in refers to inside and memb stands for across the membrane.

This proton-pumping can be modelled considering the membrane as an electric RC-circuit, while the V-ATPase can be modelled as a DC motor as represented in Figure 1. Indeed, the V-ATPase rotor can be considered to be the equivalent of a simple DC-motor rotor. The energy required by the rotor movement is generated by the energy conversion of the ATP-hydrolysis (7), while the stators rotate as gears dragged by the rotor itself. Moreover, all the DC motors convert electric energy into work with high efficiency (about 1), so, introducing this model for the rotor, the irreversibility results only in the gears. Consequently, the efficiency of the V-ATPase can be evaluated as:
\[ \eta = \frac{\Delta G_{\text{P}}}{\Delta G_{\text{ATP}}} \]
where \( \Delta G_{\text{ATP}} \) is the free energy variation due to the hydrolysis of a single ATP molecule (\(-21 \text{kJ} \text{mol}^{-1}\), being \(k_B\) the Boltzmann constant and \(T\) the temperature), \( \chi \) is the coupling ratio \( \chi = I_{\text{th}}/I_{\text{ATP}} \), being \( I_{\text{th}} \) the proton flux and \( I_{\text{ATP}} \) the ATP hydrolysis rate) and \( \Delta G_{\text{P}} \) is the free energy variation required to move the proton across the membrane:
\[ \Delta G_{\text{P}} = \Delta \phi - 2.5 \frac{RT}{F} \Delta \text{pH} \]
with \( \Delta \phi \) being the membrane potential, \( R \) is the gas constant (8.314 J mol⁻¹ K⁻¹), \( F \) is the Faraday constant (96.485 \times 10^4 A s mol⁻¹), and 2.3 \( \Delta \text{pH} \) is the physiological concentration gradient. The coupling ratio \( \chi \) is affected both by the pH gradients and by the membrane potential. The average rotation \( \bar{v} \) can be calculated as a function of the load \( r \) as:
Figure 1 | The equivalent schema for the V-ATPase system. It is a DC motor in series with a rectifier. The V-ATPase rotor can be considered to be the equivalent of a simple DC-motor rotor. The energy required by the rotor movement is generated by the energy conversion of the ATP-hydrolysis, while the stators rotate as gears dragged by the rotor itself. The DC motor converts electric energy into work with high efficiency (about 1). Consequently, the irreversibility results only in the gears.

\[ v = v(\tau) = 20 \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] \]  
(11)

Under physiological conditions, this leads to 15–20 Hz.

From these results the work dissipated in wasted heat yields:

\[ Q = T_0 S_g = W_{jc} = (1 - \eta) \Delta G_{ATP} \]

\[ = \Delta G_{ATP} - \frac{J_H}{J_{AATP}} \left( \Delta \phi - 2.3 \frac{RT_c}{F} \Delta \text{pH} \right) \]  
(12)

and the related power lost in heat flow:

\[ \dot{Q} = T_0 \dot{S}_g = \dot{W}_{jc} = (1 - \eta) \Delta G_{ATP} v(\tau) = 20 \left[ \Delta G_{ATP} - \frac{J_H}{J_{AATP}} \left( \Delta \phi - 2.3 \frac{RT_c}{F} \Delta \text{pH} \right) \right] \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] \]  
(13)

As a consequence of the previous Section it is now possible to evaluate the entropy generation due to membrane flows as:

\[ S_g = S_{g,de} + S_{g,cr} + S_{g,de} = \dot{x}_m \sum_i \frac{P_i (\mu_{i,os} - \mu_{i,ls})}{r} \tau_2 + V \tau_4 \sum_i N_i T \frac{\dot{\alpha}_i}{T} \]  
(14)

and the related entropy generation rate as:

\[ \dot{S}_g = \dot{S}_{g,de} + \dot{S}_{g,cr} + \dot{S}_{g,de} = \dot{x}_m \sum_i \frac{P_i (\mu_{i,os} - \mu_{i,ls})}{d_m} \tau_2 + V \tau_4 \sum_i N_i \frac{\dot{\alpha}_i}{T} \]  
(15)

with \( S_{g,de} \) being zero because the V-ATPase is not driven by temperature difference, and \( S_{g,cr} \) being zero because the V-ATPase is not driven by the velocity gradient.

Considering relations (14) and (15) together with relations (12) and (13) it is now possible to argue that the entropy generation, and consequently the irreversibility, depend on:

1. The chemical potential at the membrane,
2. The affinity,
3. The electric potential at the membrane,
4. The \( H^+ \)/ATP rate,
5. The pH gradient, and
6. The working temperature.

But, as highlighted in the introduction, these quantities are characteristic quantity of the thermodynamic state of a cell, which is different between normal and cancerous cells. Consequently, these quantities are also different between normal and cancerous cells of the same cell line. So, for a cancer cell it follows:

\[ \dot{Q}_c = T_0 \dot{S}_g = W_{jc} = (1 - \eta_c) \Delta G_{ATP} \]

\[ = \Delta G_{ATP} - \frac{J_H}{J_{AATP}} \left( \Delta \phi_c - 2.3 \frac{RT_c}{F} \Delta \text{pH} \right) \]  
(16)

\[ \dot{Q}_c = T_0 \dot{S}_g = \dot{W}_{jc} = (1 - \eta_c) \Delta G_{ATP} v(\tau) = 20 \left[ \Delta G_{ATP} - \frac{J_H}{J_{AATP}} \left( \Delta \phi_c - 2.3 \frac{RT_c}{F} \Delta \text{pH} \right) \right] \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau_c}{\Delta G_{ATP}} \right)^6 \right] \]  
(17)

where the significant quantities are considered different from normal cells; to indicate it, a \( c \) symbol has been introduced. As a consequence, we get a different value of the entropy generation, and the variation between a cancer cell and a normal cell leads to:

\[ T_0 \Delta S_{g,c/n} = T_0 \left( S_{g,c} - S_{g,n} \right) = \left( \frac{J_H}{J_{AATP}} \Delta \phi_c - \frac{J_H}{J_{AATP}} \Delta \phi_n \right) \]

\[ - 2.3 \frac{R}{F} \left( \frac{J_H}{J_{AATP}} T \Delta \text{pH} \right) \]  
(18)

\[ T_0 \Delta S_{g,c/n} = T_0 \left( S_{g,c} - S_{g,n} \right) = 20 \Delta G_{ATP} \left\{ \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] - \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] \right\} + \]

\[ + \left\{ \frac{J_H}{J_{AATP}} \Delta \phi \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] - \frac{J_H}{J_{AATP}} \Delta \phi \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] \right\} - \]

\[ - 2.3 \frac{R}{F} \left\{ \frac{J_H}{J_{AATP}} T \Delta \text{pH} \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] - \frac{J_H}{J_{AATP}} T \Delta \text{pH} \left[ 1 - \left( \frac{2\pi}{3} \frac{\tau}{\Delta G_{ATP}} \right)^6 \right] \right\} \]  
(19)

Furthermore, if we are able to change the entropic behaviour of the tumor cell it is possible to compel the cancer to behave as it would be a normal cell. To do so, the component \( S_{g,de} \) related to the dissipation due to work by interaction with the external field can be introduced obtaining the entropy generation (always multiplied with the environmental temperature to obtain energy balances as previously done) as:

\[ T_0 S_{g,de} = \int_0^t \left[ \sum_i J_i \cdot F_i \cdot dt \right] \]  
(20)

and the related entropy generation rate:

\[ T_0 \dot{S}_{g,de} = \left\{ \sum_i J_i \cdot F_i \cdot dV \right\} \]  
(21)

To obtain the required effect it must be:

\[ T_0 \Delta S_{g,c/n} \]

\[ T_0 \dot{S}_{g,de} = T_0 \Delta S_{g,c/n} \]

\[ T_0 \dot{S}_{g,de} = T_0 \Delta S_{g,c/n} \]  
(22)

\( \)  
(23)

The effect could be obtained by using...
1. catalysis
d. electric field interaction
e. electromagnetic or ultrasound waves,
2. molecular machines,
3. local inflow of nano-particles of ferro-fluids in interaction with a magnetic field, but this technique has yet to be designed,

and/or coupling some of these possible techniques.

Here, we want to highlight that this conceptual therapy is meant to be a supporting strategy to the currently applied anticancer therapies.

Considering the use of magnetic fields it is possible to argue that any such field would modify the rotation of the diseased cell towards the normal one. So, it must induce an electric field strong enough to obtain the normal rotation of the rotor. That means, the frequency of the electric field must be such that:

\[
\Delta \nu = 20 \left( \frac{2\pi \cdot \tau_c}{3 \cdot \Delta G_{\text{ATP}}} \right)^6 \left( \frac{2\pi \cdot \tau}{3 \cdot \Delta G_{\text{ATP}}} \right)^6
\]

and it would supposedly be in the 0 \div 40 Hz range, which is twice the physiological one and this will not damage the normal cell(s). The torque can be related to the membrane potential and results in values of the order of \(10^{-21}\) Nm. Now, this leads us to consider that this torque can be obtained also as: 

\[
\tau \approx qEd_c
\]

and that the relation between the electric field and a magnetic field for an electromagnetic wave is:

\[
B = \sqrt{\mu_m \varepsilon_c E}
\]

with \(\mu_m\) being the magnetic permeability and \(\varepsilon_c\) representing the electric permittivity of the cell membrane.

Considerations. All types of ATPases, i.e., the A-ATPase of Archaea, the E-,F-,P- and the V-ATPases are essential for life and all of them generate an electrochemical ion gradient across the membrane and hydrolyse or synthesize ATP. Also, from a structural point of view, they are similar; indeed, they are enzymatic complexes, which work as molecular rotary motors. In particular, V-ATPase plays an important role in receptor-mediated endocytosis, in intracellular transports, and in the acidification of late endosomes.

Metabolism is a cycle composed of a continuous sequence of oxidations and reductions. Considering our DC motor approach, the electromotive force is the free energy variation, \(\Delta G_{\text{pump}}\) required to move the proton across the membrane represented by the Nernst equation (10). From this equation it is possible to highlight that any such field would modify the rotation of the diseased cell towards the normal one.

Four regulatory mechanisms are known:

1. The regulation of pump density, useful to maintain their cytoplasmic and vacuolar pH stable;
2. The regulation of \(V_1\) and \(V_0\) domain association/dissociation;
3. The regulation of secretory activity, thereby maintaining the balance in the formation of bisulfite and binding efficiency between \(H^+\) and the pump;
4. The modifications of the membrane potential due to electrogenic force.

Using a thermodynamic approach, the aim of this paper is to highlight how external electromagnetic waves can modify the mechanical behaviour of the V-ATPase rotor. So, now, we must evaluate the intensity and the frequency of the applied external magnetic field to obtain some beneficial anticancer effects yet without endangering the patient. To do so, we consider that any breakdown in the rotor can be modelled as a difference \(\Delta \tau\) in the torque in comparison with the normal value \(\tau\), such that:

\[
\tau_c = \tau + \Delta \tau
\]

By using this last relation in equation (22) it follows that

\[
\tau + \Delta \tau = q(E + \Delta E) \cdot d_c
\]

with \(E + \Delta E\) denoting the electric field related to the breakdown of the V-ATPase rotor. Consequently, the effect of an external magnetic field must be to contrast this field variation, so that, considering relation (26), it follows:

\[
B = \Delta E \sqrt{\mu_m \varepsilon_c}
\]

Now, considering a torque variation for the breakdown in the order of \(0 \div 3\) pN nm\(^{-1}\), so that the magnetic permeability is about the value of the permeability in the air, \(\mu_m \approx 10^{-6}\) H m\(^{-1}\), and so that the electric permeability is around \(\varepsilon_c \approx 10^{-6} \div 10^{-5}\) F m\(^{-1}\), \(\sqrt{\mu_m \varepsilon_c} \approx 10^{-12} \div 10^{-14}\) m\(^{-1}\) and that the electric field at the membrane is around \(10^7\) V m\(^{-1}\) it follows that the therapeutic magnetic field must be of the order of \(10^{-7} \div 10^{-4}\) T, i.e., of the same order as the Earth’s magnetic field.

Now, from relation (24) we can obtain the possible range of frequencies of the magnetic wave. Considering that the normal value of the torque is around \(10\) pN nm\(^{-1}\), we assume a torque variation for the breakdown of the order of \(0 \div 3\) pN nm\(^{-1}\); so, it is possible to obtain a frequency range of the order \(0 \div 10\) kHz for therapeutic use.

Moreover, this frequency can be confirmed by evaluating the time \(\tau_2\) related to the diffusion current driven by chemical potential gradients. It can be calculated by considering the macroscopic phenomenon of diffusion across the membrane as:

\[
\tau_2 \approx \frac{d}{D}
\]

with \(d \approx 10^{-8}\) m being the length of the membrane and \(D\) the diffusion coefficient. Considering that the diffusion coefficient of the ions across a membrane is around \(10^{-12} \div 10^{-8}\) m\(^2\) s\(^{-1}\), it follows \(\tau_2 \approx 10^{-4} \div 1\) s, which is equivalent to a frequency \(v = 1/\tau_2\) of \(0 \div 10\) kHz.

Conclusions

Proteins play a fundamental role in ion transport because membranes represent a barrier to free diffusion of molecules.

In active transport an ion crosses the membrane against its electrochemical potential. The required energy for this process is obtained by the chemical energy released from hydrolysis of ATP, or pyrophosphate, or from the movement of a co-transported or coupled ion along its electrochemical gradient. Indeed, the coupled
downhill and uphill movement of ions is a common transport path through the membrane. In this context, the role of the pumps is fundamental, with particular regards to V-ATPase, i.e., the pump managing the H⁺ transport. Indeed, it moves positive charges into and from the cytoplasm through the hydrolysis of ATP, with the consequence of establishing a large membrane voltage (inside negative and outside positive) and, consequently, a pH gradient of about 400 mV for H⁺. The V-ATPase is composed of a membrane extrinsic and a membrane intrinsic sector, and couples catalysis of ATP hydrolysis to proton transport by a rotational mechanism. V-ATPase is fundamental in the analysis of cell behavior because the H⁺ gradient established by this molecular pump is used to drive coupled active movements of other ions across the cell membrane. One example is the Cl⁻ transport: indeed, Cl⁻ is actively transported across the membrane because the membrane potential is more negative than the equilibrium potential for this ion.

The ion channels and transporters provide different permeability to distinct ions, such as Na⁺, K⁺, Ca²⁺, and Cl⁻. As a consequence of the asymmetry in these ion distributions, a membrane potential exists between the cytoplasm and the extracellular environment. It is expressed relative to the extracellular environment and a cell depolarizes if the membrane potential is relatively less negative, and vice versa. The membrane potential can be calculated by using the Goldman–Hodgkin–Katz equation:

$$\Delta \phi = \frac{RT \ln \left( \frac{P_{Na^+} [Na^+]_{out}}{P_{K^+} [K^+]_{out} + P_{Cl^-} [Cl^-]_{out}} \right)}{F} + \frac{RT \ln \left( \frac{P_{K^+} [K^+]_{out}}{P_{Na^+} [Na^+]_{out} + P_{Cl^-} [Cl^-]_{out}} \right)}{F}$$

where $P$ is the permeability of the ion, $[A]$ means concentration of the A-ion, $R$ is the ideal gas constant (8.314 J mol⁻¹ K⁻¹), $T$ is the temperature, and $F$ is the Faraday constant (96.485 x 10⁻³ A/s mol⁻¹). From relation (31) it is possible to state that the membrane potential can be changed by alterations in the conductance of one or more ions. In particular, from the previous considerations on the V-ATPase we can highlight that this pump can change the transport of H⁺ and, as a consequence of the Cl⁻–H⁺ coupled transport, it can change the Cl⁻-transport. Consequently, both the membrane potential and the pH are changed by any alteration of the V-ATPase.

It is noteworthy that in the analysis of the mitotic activities in sarcoma cells, the membrane potential was found to undergo hyper-polarization before entering M phase. It suggests that the level of $\Delta \phi$ is correlated with cell cycle progression. Moreover, membrane hyper-polarization was shown to block reversibly DNA synthesis and mitosis and to be correlated with the level of differentiation. Consequently, the membrane potential represents a fundamental quantity for the control of critical cell functions, particularly, with regards to proliferation, migration, and differentiation. To support this conclusion, some experimental evidence can be cited: First, direct in vitro and in vivo comparisons of the membrane potentials have highlighted that cancer cells are more depolarized in relation to normal cells; some evidence of this electrochemical behavior of the cancer cells can be summarized as follows: between normal and cancerous breast cells, hepatocytes and hepatocellular carcinoma cells, normal and neoplastic adenocortical tissues, normal embryonic fibroblasts and fibrosarcoma cells, benign and cancerous skin cells, and between normal and cancerous ovarian tissue cells.

Lastly, cell migration is controlled by the movement of ions and water in that an acidic environment furthers this phenomenon. This environmental pH is regulated by the H⁺ concentration, which is related to the V-ATPase functions. In addition, the membrane potential is considered an indirect factor of cell migration, strictly related to the electrical driving force for Ca²⁺ whereas a hypopolarized membrane potential increases intracellular Ca²⁺ through the TRP channels; in contrast, membrane depolarization activates the Ca²⁺ channels. Notably, migrating cells have a high intracellular Ca²⁺ concentration gradient.

In summary, all these findings highlight that V-ATPase-mediated control of the cell membrane potential and that of the environmental pH can potentially represent a valuable support strategy for anticancer therapies. In here, a constructual approach has been used to study how V-ATPase can be modulated for therapeutic purposes. In particular, V-ATPase can be regulated by using external fields, such as electromagnetic fields, and we have introduced a theoretical approach to quantify the appropriate field strength and frequency for this new adjuvant therapeutic strategy. Here, in contrast with the usual applications of constructual theory, the flows have been assessed by evaluating the entropy generation because its variation is strictly related to the flows across the cell membrane.
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Author contributions
U.L. developed the thermodynamic approach. U.L., A.P. and T.S.D. contributed to the main manuscript text. All authors (U.L., A.P., T.S.D.) reviewed the manuscript.

Additional information
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