Global cognitive function and processing speed are associated with gait and balance dysfunction in Parkinson’s disease

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Abstract

Background: Our primary objective was to determine the relationship between global cognitive function and specific domains of gait and balance in a cohort of Parkinson’s disease (PD) subjects. In a secondary analysis, we determined whether specific cognitive domains correlated with gait and balance performance.

Methods: Fourteen PD subjects (mean age 61.1 ± 7.8 years) were recruited from the Rush University Medical Center Movement Disorders clinic. Subjects underwent clinical assessment using the motor subsection of the Unified Parkinson’s Disease Rating Scale (UPDRS) followed by quantitative gait and balance assessments using the APDM Mobility Lab™ system (Mobility Lab, APDM Inc., Portland, OR). Subjects completed global cognitive testing using the Mattis Dementia Rating Scale (MDRS) as well as domain specific cognitive measures. Spearman’s rho was used to assess correlations between cognitive measures and gait and balance function, with False Discovery Rate (FDR) correction for multiple comparisons.

Results: Global cognitive function had the strongest correlation with stride velocity ($r = 0.816, p = 0.001$), turn duration ($r = -0.806, p = 0.001$), number of steps to turn ($r = -0.830, p = 0.001$), and mean velocity of postural sway in the medio-lateral direction ($r = -0.726, p = 0.005$). A significant correlation was found between processing speed and two turning measures (turn duration, $r = -0.884, p = 0.001$; number of steps to turn, $r = -0.954, p < 0.001$), but no other associations were found between specific cognitive domains and gait domains.

Conclusions: This pilot study provides preliminary data regarding the association between global cognitive function and pace-related measures of gait, turning, and postural sway. Furthermore, reduced processing speed was found to be associated with difficulty in performing turns.

Keywords: Parkinson’s disease, Cognition, Processing speed, Gait, Turning

Background

Difficulties with gait and balance in Parkinson’s disease (PD) increase the risk of falls, institutionalization, and death [1–3]. Research studies have established that safe ambulation requires cortical input from areas involved with higher cognitive function [4, 5]. Cognitive impairment, especially prefrontal lobe dysfunction, has been linked to motor disability in PD but these relationships remain unclear [5–7].

Clinical rating scales, such as the Unified Parkinson’s disease Rating Scale (UPDRS) [8], and measures derived from such scales, such as the postural instability/gait disturbance (PIGD) score, have been used to examine the relationship between cognitive and motor impairment [9]. However, these clinical scales are subject to rater judgment and provide only limited detail because the ordinal fixed scores (0–4) force raters into a limited number of item choices without the ability to quantify disease impairment or disability as continuous measures. Thus far, these clinical scales have had limited ability to elucidate the relationship between cognition and gait and balance [10].

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Body-worn inertial sensors can provide a multitude of continuous, objective measures of gait and balance [11–13]. Wearable technology allows for measurement and replication of relationships between gait and cognition without the confounding factors of heightened attentional load and observer effect seen in the laboratory [14]. Moreover, these quantitative measures can be categorized into specific domains of gait and balance for analysis [11]. In this pilot project, we used the APDM Mobility Lab™ (Mobility Lab, APDM Inc., Portland, OR), a valid and reliable measurement tool of gait and balance [15–17], to examine motor function in a small cohort of PD subjects. Our primary objective was to determine whether global cognitive function correlated with specific domains of gait and balance. Through a secondary analysis, we assessed whether specific cognitive domains correlated with gait and balance performance.

Methods

This cross-sectional study involved PD subjects recruited from the Rush University Medical Center (RUMC) Movement Disorders clinic. The study proposal and consent were approved by the Institutional Review Board of Rush University and met standards for ethical human research. All PD patients met the UK Parkinson’s disease society brain bank clinical diagnostic criteria [18] and the diagnosis of PD was confirmed by a movement disorders neurologist through personal interview, medical history, physical examination, and chart review.

Clinical and demographic data included age at time of enrollment, age of onset, disease duration, height, and weight. Disease severity was assessed for each subject using the motor subscale of the UPDRS (UPDRS-III) [8] and Hoehn and Yahr (H&Y) [19] staging in the ON medication condition. PIGD scores were calculated using the arithmetic sum of items 13, 14, 15, 29, 30 of the UPDRS [20].

The instrumented walk (i-WALK) and instrumented sway (i-SWAY) test protocols [21, 22] were performed using the commercially available APDM Mobility Lab™ six inertial sensor system (Mobility Lab, APDM Inc., Portland, OR), a sensitive, valid and reliable measurement tool of gait and balance in the PD population [15, 17]. The sensors were attached 4 cm above each malleolus, at the dorsum of the wrists, on the lumbar trunk at the level of L5, and on the upper trunk 2 cm below the sternal notch. The i-WALK protocol consisted of the subject walking back and forth continuously between two points 25 ft apart for a period of two minutes while in the ON medication condition. All subjects performed the i-WALK without an assistive device and the mean value for each gait parameter was calculated. A total of 23 measures were computed and categorized into four domains: pace, arm and trunk movement, dynamic stability, and turning (Appendix) [23]. Subjects then completed the i-SWAY, during which they stood still with their hands across their chest and their feet shoulder width apart or together and their eyes opened or closed. The protocol consisted of measuring balance with the feet together, eyes closed, to maximize the sensitivity of the balance testing. All assessments were completed in the ON medication condition.

After completing the i-WALK and i-SWAY, subjects rested for approximately 1–2 h. Then, a neuropsychologist administered the Mattis Dementia Rating Scale (MDRS) [24, 25], a test of global cognitive function. Subjects also completed neuropsychological measures for the following domains: verbal fluency, verbal memory (immediate and delayed), processing speed, working memory, and executive function (See Table 1).

SPSS version 16.0 was used for statistical analysis. Spearman’s rho (r) was used to assess correlations between MDRS scores and measures of gait and balance, as well as to assess correlations between the domain-specific cognitive tests and gait and balance measures. Raw scores from each neuropsychological test were converted to z scores. Multiple comparisons were accounted for by using a false discovery rate (FDR) adjustment [26] α = 0.05 [20]. FDR was considered more appropriate than the more conservative corrections, such as Bonferroni, as a large number of associations were under investigation [26, 27].

Results

Fourteen subjects with PD were included in the analysis (Table 2). Subjects had a mean age of 61.1 ± 6.1 years and disease duration of 12.7 ± 6.2 years. Mean motor UPDRS was 21.5 ± 9.2 (ON condition) indicating that subjects had mild to moderate disease severity. The mean MDRS Total score was 132.2 ± 8.3, indicating that subjects varied between largely intact cognition and mild cognitive impairment. The MDRS Total score had the strongest correlation with pace-related measures of gait, turning, and postural sway in the ON condition (Table 3). Significant correlations were found between MDRS Total scores and stride velocity (r = 0.816, p = 0.001), turn duration (r = −0.806, p = 0.001), and number of steps to turn (r = −0.830, p = 0.001). MDRS Total scores correlated with one balance measure, mean sway velocity in the medio-lateral direction (r = −0.726, p = 0.005). MDRS Total scores had a modest correlation with motor UPDRS scores in the ON condition (r = −0.568, p = 0.043). There was no significant correlation between MDRS Total scores and PIGD scores.
Lastly, an association was found between processing speed, as measured by the SDMT, and two measures from the gait turning domain (turn duration and number of steps to turn), but no other cognitive domain had significant correlations with any gait domains (Table 4).

**False discovery rate (FDR)**

A total of 161 correlations were performed. After FDR correction, 26 significant associations (Spearman’s rho > 0.2, \( p < 0.05 \)) was reduced to six significant associations (bolded in Tables 1 and 2).

**Discussion**

This pilot study adds to the body of evidence [5, 7, 28–30] that lower global cognitive function is correlated with worse performance in different domains of gait and balance. Importantly, this is the first study to demonstrate the correlation between reduced processing speed and impaired turning. Though this is a small pilot study, the validity of our results are strengthened by the strong reliability of the APDM system ([15–17, 31]. Salarian et al. [31] demonstrated that the APDM Mobility lab system has high test-retest reliability for turn duration (\( \rho = 0.89 \)) and good reliability for the number of steps to turn (\( \rho = 0.75 \)).

Prior studies [32] have shown that executive function plays a role in turning, but the domain of executive function may be too broad to provide meaningful results in a clinical or research context [33]. Processing speed is a more precise construct as it is a basic cognitive process that subserves higher-order cognitive domains such as executive function [34]. The mechanism of reduced processing speed in...
Table 4: Correlation of Gait and Balance Domains with Specific Cognitive Domains

| Language          | Verbal Memory – Immediate | Verbal Memory – Delayed | Processing Speed | Working Memory | Executive Function |
|-------------------|---------------------------|-------------------------|------------------|---------------|--------------------|
|                   | COWAT [51]                | RAVLT Trial 5 [52, 53]  | RAVLT Delayed Recall [52, 53] | SDMT [54]     | ACT [55, 56]       | TOL [57]        |
|                   | r                          | r                       | r                 | r             | r                  | r              |
|                   | p                          | p                       | p                 | p             | p                  | p              |
| **Gait – pace**   |                           |                         |                   |               |                    |                |
| Gait cycle time, sec | –0.624 0.040          | −0.402 0.221            | −0.291 0.385      | −0.573 0.083  | −0.219 0.571       | 0.256 0.507    |
| Cadence, steps/min | 0.574 0.065            | 0.420 0.198             | 0.291 0.385       | 0.530 0.115  | 0.310 0.416        | −0.183 0.638   |
| Stride velocity, %/s | 0.492 0.124          | 0.525 0.097             | 0.517 0.103       | 0.744 0.014  | 0.529 0.143        | 0.146 0.708    |
| Stride length, %h  | 0.091 0.790           | 0.388 0.238             | 0.467 0.148       | 0.585 0.075  | 0.785 0.012        | 0.602 0.086    |
| RoM leg, deg      | 0.091 0.790           | 0.388 0.238             | 0.467 0.148       | 0.585 0.075  | 0.785 0.012        | 0.602 0.086    |
| **Gait – arm & trunk Movement** |                   |                         |                   |               |                    |                |
| Arm peak velocity, deg/s | 0.374 0.258         | 0.370 0.263             | 0.342 0.304       | 0.744 0.014  | 0.347 0.360        | 0.091 0.815    |
| Arm swing RoM, deg | −0.469 0.145         | −0.498 0.119             | −0.199 0.558      | 0.085 0.815  | −0.183 0.638       | −0.018 0.963   |
| Asymmetry arm swing RoM, % | −0.542 0.085      | −0.438 0.177             | −0.231 0.494      | −0.311 0.382  | −0.237 0.539        | −0.146 0.708   |
| ROM trunk frontal plane, deg | 0.287 0.392        | 0.128 0.708             | 0.217 0.521       | 0.335 0.343  | 0.639 0.064        | 0.475 0.197    |
| RoM trunk sagittal plane, deg | 0.082 0.811      | −0.096 0.779             | 0.000 1.000      | 0.598 0.068  | 0.347 0.360        | 0.110 0.779    |
| RoM trunk horizontal plane, deg | −0.369 0.264     | −0.233 0.491             | −0.037 0.914      | 0.024 0.947  | 0.091 0.815        | 0.183 0.638    |
| **Gait – Dynamic Stability** |                   |                         |                   |               |                    |                |
| Double support time, % of gait cycle | −0.292 0.384 | −0.324 0.331             | −0.393 0.232      | −0.378 0.281  | −0.548 0.127        | −0.420 0.260   |
| Stance time, % of gait cycle | −0.292 0.384 | −0.324 0.331             | −0.393 0.232      | −0.378 0.281  | −0.548 0.127        | −0.420 0.260   |
| **Turning**       |                           |                         |                   |               |                    |                |
| Peak velocity, deg/s | 0.273 0.416         | 0.548 0.056             | 0.542 0.069       | 0.732 0.016  | 0.649 0.042        | 0.389 0.266    |
| Duration, sec     | −0.597 0.053         | −0.643 0.024             | −0.712 0.009      | 0.000 1.000  | −0.884 0.001        | −0.621 0.055   |
| Mean step time, sec | −0.433 0.184    | −0.119 0.728             | 0.032 0.925       | −0.354 0.316  | −0.164 0.673        | 0.347 0.360    |
| Number of steps, n | −0.409 0.212        | −0.700 0.016             | −0.400 0.198      | −0.954 0.001  | −0.803 0.009        | −0.566 0.112   |
| **Postural sway** |                           |                         |                   |               |                    |                |
| Sway RMS AP, m/s²  | −0.410 0.210         | −0.366 0.243             | −0.400 0.198      | −0.220 0.542  | −0.382 0.276        | −0.464 0.176   |
| Sway RMS ML, m/s²  | −0.255 0.449         | −0.443 0.149             | −0.556 0.061      | −0.122 0.737  | −0.580 0.079        | −0.580 0.079   |
| Mean velocity AP, m/s | −0.059 0.863     | −0.460 0.132             | −0.025 0.939      | −0.085 0.815  | 0.096 0.793         | 0.096 0.793    |
| Mean velocity ML, m/s | −0.410 0.210    | −0.633 0.027             | −0.609 0.036      | −0.256 0.475  | −0.574 0.083        | −0.437 0.207   |
| Centroidal frequency AP, Hz | −0.027 0.936    | −0.341 0.278             | −0.513 0.088      | 0.061 0.867  | −0.615 0.059        | −0.737 0.015   |
| Centroidal frequency ML, Hz | 0.077 0.821    | −0.429 0.164             | −0.517 0.085      | 0.091 0.802  | −0.362 0.304        | −0.608 0.062   |

*Bolded measures indicate measures that remained significant after False Discovery Rate (FDR) correction*

Controlled Oral Word Association Test (COWAT) [51], Rey Auditory Verbal Learning Test (RAVLT) [52, 53], Symbol Digit Modalities Test (SDMT) [54], Auditory Consonant Trigrams (ACT) [55, 56], Tower of London (TOL) [57]
PD has been explored in several studies. Jokinen et al. [35] used \(^{18}\text{F}\text{]fluorodopa (Fdopa) Positron Emission Tomography (PET) to demonstrate that reduced Fdopa uptake in the anterior cingulate gyrus, thalamus, and caudate nucleus was related to decreased processing speed. Likewise, when examining the predictive role of gray and white matter fractional anisotropy on processing speed in PD subjects and controls, Price et al. [36] found that lower prefrontal fractional anisotropy and caudate nucleus volume were related to reduced processing speed in PD subjects. Thus, dopaminergic dysfunction in networks connecting the striatum and prefrontal cortex and caudate volume loss and dysfunction may be involved in the lower processing speed observed in PD [35, 37–39].

Identification of processing speed deficits is particularly important since this construct has the potential to be modified with cognitive training [40–46]. Edwards et al. [41] demonstrated that PD subjects could improve cognitive processing speed over a three-month period through a self-administered task using speed of processing training (SOPT) software (InSight). Moreover, Milman et al. [47] enrolled 18 PD subjects in a 12-week, computerized cognitive remediation program and found that subjects improved in both gait turning speed and duration. Additional studies are needed to replicate these results and determine whether such cognitive training methods could translate to improved gait, turning, balance, or other activities of daily living (ADLs) in PD.

This study also demonstrated that pace-related measures of gait and postural sway were correlated with global cognitive scores. We were unable to determine the cognitive domain(s) driving this association, likely due to our small sample size. However, prior studies do provide some insight into the cognitive basis for dysfunction in the pace and postural sway domains in PD. Amboni et al. [48] conducted a study in 43 PD subjects and 20 healthy controls that examined the associations between cognition and motor function using an automated sensor-based system generating eight measures categorized into two domains: (1) gait pace and (2) postural stability or balance. Results showed that reduced visuospatial processing was associated with worse postural stability and supported previous studies that describe the importance of processing of visual information for locomotion and motor planning, particularly in PD [49, 50].

In addition to visuospatial function, working memory may also play a role in postural stability. In a cohort of 121 early PD subjects and 184 healthy controls, Lord et al. [51] examined the associations between cognition and motor function using an instrumented walkway system (GAITRite, CIR systems, USA) that generated 16 different gait and balance measures. Results showed a significant association between postural stability and working memory in PD subjects with the PIGD subtype. It was hypothesized that changes in postural stability may be a marker of amnestic features, and that reduced working memory may reflect cortical amyloid deposition in the PIGD subtype of PD [51, 52].

Studies have also suggested a possible relationship between the domain of gait pace and attention [51, 53, 54]. Gait is a goal directed activity, and the finding that attentional circuits are activated through dopaminergic and cholinergic signaling between the dorsolateral prefrontal cortex and the caudate nucleus during gait performance [55] supports this hypothesis. In early PD, individuals may be able to compensate for pace deficits by relying more heavily on these attentional circuits [56]. However as the disease progresses and attentional circuitry becomes increasingly abnormal [57], PD patients are likely less able to compensate [56] and have reduced pace as a result [51].

The strengths of our study include the use of quantitative, sensor-based assessments to evaluate gait and balance that provided objective metrics of motor function, as well as a neuropsychological testing protocol that included global and domain specific cognitive measures. The limitations of our study include a small sample size and the use of only one neuropsychological test per cognitive domain. We also did not include a control group, which would have been helpful in determining which relationships are directly related to PD compared with normal aging. Despite these limitations, our findings highlight the value of linking quantitative motor assessments with clinical neuropsychological measures to elucidate the complex interplay between motor and cognitive function in PD. Overall, this study demonstrates that there is a relationship between specific cognitive domains and motor function in PD which warrants further exploration. We showed that impaired turning is associated with reduced processing speed and larger studies are needed to validate these findings. The question of whether cognitive deficits mediate gait and balance dysfunction or vice versa, or whether there is an interaction between the two processes is an area of active research investigation in PD and other neurodegenerative disorders [7].

**Conclusions**

This is the first study to demonstrate the correlation between reduced processing speed and impaired turning in Parkinson’s disease. Identification of processing speed deficits is particularly important since this construct has the potential to be modified with cognitive training. Further studies are needed to validate these findings.
## Appendix

**Table 5** Gait and balance domains with the corresponding instrumented measures [11]

| Instrumented Measure | Unit of Measure | Definition |
|----------------------|-----------------|------------|
| Gait–pace            |                 | Pace during straight ahead walking |
| Gait cycle time      | s               | Duration of a complete gait cycle |
| Cadence              | steps/min       | Stepping rate |
| Stride velocity      | %h/s            | Average gait speed normalized for height |
| Stride length        | %h              | Distance between 2 consecutive heel-strikes normalized for height |
| RoM leg              | °               | Range of motion (RoM) of the leg (calculated from the integrated sagittal angular velocity, approximation of step length) Average of the left and right sides |
| Gait–arm & trunk movement |               | Arm and trunk movement during straight-ahead walking |
| Arm peak velocity    | °/s             | Peak (95 %) angular velocity of most affected arm |
| Arm swing RoM        | °               | Range of motion of most affected arm during arm swing |
| Asymmetry arm swing RoM | %          | Average asymmetry of left and right arm swing range of motion |
| RoM trunk frontal plane | °            | Average range of motion of trunk in frontal plane |
| RoM trunk sagittal plane | °            | Average range of motion of trunk in sagittal plane |
| RoM trunk horizontal plane | °        | Average range of motion of trunk in horizontal plane |
| Gait–dynamic stability |               | Dynamic stability during straight-ahead walking |
| Double support time  | % of gait cycle | Percentage of a gait cycle that both feet are on the ground |
| Stance time          | % of gait cycle | Average percentage of a gait cycle that either foot is on the ground |
| Swing time           | % of gait cycle | Average percentage of a gait cycle that either foot is off the ground |
| Turning              |                 | 180° turn |
| Peak velocity        | °/s             | Peak (95 %) angular velocity of trunk during turning |
| Duration             | s               | Duration of a 180° turn |
| Mean step time       | s               | Average duration of step during 180° turn |
| Number of steps      | n               | Total number of steps during 180° turn |
| Postural sway        |                 | Standing quietly for 30 s |
| Sway RMS AP          | m/s²            | Root mean square (RMS) of acceleration time series in anteroposterior (AP) direction |
| Sway RMS ML          | m/s²            | Root mean square of acceleration time series in mediolateral (ML) direction |
| Mean velocity AP     | m/s             | Mean velocity of center of pressure in anteroposterior direction |
| Mean velocity ML     | m/s             | Mean velocity of center of pressure in mediolateral direction |
| Centroidal frequency AP | Hz             | Centroidal frequency in anteroposterior direction; variability of the acceleration traces power ranging from 0 to 1 |
| Centroidal frequency ML | Hz             | Centroidal frequency in mediolateral direction; variability of the acceleration traces power ranging from 0 to 1 |

Nomenclature: *°* degree, *g* acceleration of gravity, *%h* percentage of patient’s height, *n* number, *m/s²* acceleration, *s* seconds, – dimensionless
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Availability of data and materials
The datasets during and/or analyzed during the current study available from the corresponding author on reasonable request.

Authors’ contributions
Gian Pal (GP), Joan O’Keefe (JO), Erin Robertson (ER), Bryan Bernard (BB), Sharlet Anderson (SA), Deborah Hall (DH). Research project: A. Conception: GP, B. Organization: GP, DH, C. Execution: GP, JO, ER, BB, SA, DH. Statistical Analysis: A. Design, Execution, Review and Critique: GP, JO, ER, BB, SA, DH. Manuscript Preparation: A. Writing of the first draft: GP, B. Review and Critique: GP, JO, ER, BB, SA, DH. All authors read and approved the final manuscript.

Competing interests
The authors declare that they have no competing interests.

Consent for publication
Individual patient data is not presented so this is not applicable.

Ethics approval and consent to participate
The study proposal and consent were approved by the Institutional Review Ethics approval and consent to participate.

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