Utility of brain parenchyma density measurement and computed tomography perfusion imaging in predicting brain death

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Abstract

Purpose: To assess the utility of brain parenchyma density measurement on unenhanced computed tomography (CT) in predicting brain death (BD), in order to evaluate the added value of CT perfusion (CTP).

Material and methods: A total of 77 patients who were clinically diagnosed as BD and had both CT angiography (CTA) and CTP imaging in the same session were retrospectively reviewed. On unenhanced phase of CTA, density measurement was performed from 23 regions of interests (ROIs) which were located in the following areas: level of basal ganglia (caudate nucleus, putamen, corpus callosum, posterior limb of internal capsule), level of brainstem, grey-white matters on levels of centrum semiovale (CS), high convexity (HC), and cerebellum. CTP images were evaluated qualitatively and independently. Grey matter (GM), white matter (WM), density, and GM/WM density ratio of BD patients were compared with control subjects.

Results: Comparing with the normal control group, the GM and WM density at each level and GM/WM density ratio of CS, HC, and cerebellum level were significantly lower in brain-dead patients (p = 0.019 for HC-WM, p < 0.001 for other areas). Using ROC analysis, the highest value of area under curve (AUC) for the GM/WM density ratio was found at the HC level (AUC = 0.907). The sensitivity of the GM/WM density ratio at the HC level was found to be 90% when the cut-off value of 1.25 was identified. Evaluating the GM/WM density ratio together with the CTP results increased the sensitivity further to 98%.

Conclusions: The GM/WM density ratio at the HC level on unenhanced CT may be a useful finding to predict BD. Also, the addition of CTP increases the sensitivity of this method.

Key words: brain death, computed tomography angiography, computed tomography perfusion, density.

Introduction

The algorithm of brain death (BD) diagnosis occurs on the basis of clinical findings and neurological examination, which is followed by ancillary tests, especially when confounding factors (e.g. metabolic and endocrine disturbances, sedative drugs) could affect the clinical evaluation [1]. Computed tomography angiography (CTA) has been accepted as one of the ancillary tests and is commonly used for the confirmation of cerebral circulatory arrest in BD [2]. In addition, computed tomography perfusion (CTP) is known to be a highly sensitive method in the diagnosis of BD by showing the lack of cerebral perfusion [2-4].

Unenhanced CT findings of BD have been previously described as diffuse cerebral oedema, loss of distinction between grey matter (GM) and white matter (WM), and herniation [5]. Cerebral oedema occurs as a result of increase in water content of GM and is mainly responsible for the reduction of attenuation in the cerebral cortex on CT imaging [6-8]. In two studies conducted by Inamasu et al.,
the role of loss of GM-WM discrimination in predicting the prognosis after cardiac arrest was investigated, and it was shown that this sign could be related to poor outcome [9,10]. In addition, there are various studies evaluating the prognostic value of the GM/WM ratio as a quantitative method in comatose patients after cardiac arrest [11-17]. According to the American Heart Association guidelines for post-cardiac arrest care, the presence of a significant decrease of GM/WM ratio could be used as a predictor of poor outcome in patients with coma, who are not treated with hypothermia [18].

In routine clinical practice, comatose patients are evaluated cautiously for signs of BD. Nevertheless, it is also critical to have a reliable and accurate method that could predict BD in such patients at early stages, especially for organ donation. For this reason, a few studies have shown the relationship between BD and GM-WM density changes [19,20]. However, a study that evaluated unenhanced CT and CTP for the prediction of BD has not been reported, to our knowledge. In this study, we aimed to evaluate the effectiveness of density measurement from various regions on unenhanced CT scan and the contribution of CTP in predicting BD.

**Material and methods**

**Study population**

The study protocol was approved by our institutional review board. Written informed consent was waived due to the retrospective nature of this study. Between September 2014 and July 2018, 92 patients who underwent CT after clinical diagnosis of BD were collected from our database. Inclusion criteria were patients with clinically diagnosed BD and who had CTA and CTP obtained with BD protocol. After the exclusion of nine patients without CTP images, five patients with unenhanced CT images that were unsuitable for density measurement due to the artifacts, and one patient with an extensive extracalvarial herniation after decompressive craniectomy, 77 patients were enrolled in the study. The control group was retrospectively collected from the PACS database, including age- and sex-matched patients who had an unenhanced CT scan without evidence of ischaemia, intracranial haemorrhage, neoplastic lesion, or parenchymal disease. A flow chart of the study is shown in Figure 1.

**Computed tomography protocol and density measurements on unenhanced computed tomography**

All CT examinations were acquired with a 128-detector (Siemens Somatom Definition AS, Munich, Germany) or 64-detector (Toshiba Aquilion, Tokio, Japan) CT scanner (64 vs. 13 patients, respectively). The acquisition parameters were slice thickness of 1 mm, pitch 0.55, 100 kV, 200 mAs, 220 FOV, and 512 × 512 matrix in our routine BD protocol. Despite the fact that this protocol includes two-phase CTA (arterial phase scan at the 20th and venous phase scan at the 60th second after contrast administration), only unenhanced scans were evaluated in this study. CT scans were performed within 2-12 hours of clinical examination of BD. In the control group, unenhanced CT images were obtained with standard head CT protocol with a slice thickness of 5 mm at either 128-detector or 64-detector CT scanner (67 vs. 10 subjects, respectively). All density measurements of the patient group were performed by two radiologists (H.S. and A.A.), independently, who were blinded to measurements of each other. The measurements of the senior radiologist (H.S.) with 10 years of experience in the assessment of CTA for BD confirmation were accepted as the reference standard. CT images of the control group were measured by the other radiologist (A.A.).

Circular region of interests (ROIs) were placed in several areas in brain parenchyma, which were first described by Torbey et al. [11] and modified by Vigneron et al. [19]. In this study, two different places were added, and Hounsfield unit (HU) measurements were taken from each of 23 ROI in the following areas (Figure 2):

- Level of basal ganglia (BG): caudate nucleus (CN), putamen (PU), corpus callosum (CC), and posterior limb of internal capsule (PIC) were included. The GM to WM ratio was calculated according to the following method, which was described in previous studies [8,12-14]:
  \[
  \text{GW/WM density ratio (BG)} = \frac{\text{CN} + \text{PU}}{\text{CC} + \text{PIC}}.
  \]
- Level of centrum semiovale (CS): GM and WM of each hemisphere were measured 5 mm above the level of CG and average values of HU were calculated.
- Level of high cerebral convexity (HC): GM and WM of each hemisphere were measured 5 mm above from level

...
of CS and averaged. ROIs were placed to medial parts of the brain parenchyma in order not to be affected by beam hardening artifact on both HC and CS levels.

- Level of cerebellum: GM and WM of each hemisphere were measured and averaged.
- Level of brain stem (BS): midbrain, pons, and medulla oblongata were measured from the middle part with an ROI cursor of 20 mm² differently from other levels, which were calculated with 10 mm² circular ROI.

In both patient and control groups, the mean HU values of WM, GM, and GM/WM density ratio were recorded at each level. However, regions that could not be evaluated due to the remarkable haemorrhage, infarct, shift, or artifacts were not included in the analysis in the patient group.

Computed tomography perfusion protocol and interpretation

CTP images were obtained with a bolus of contrast media (40 ml) 10 minutes after CTA in our routine BD protocol. CTP scan was performed between the level of internal carotid artery bifurcation and superior edge of lateral ventricles with a section thickness of 10 mm and a total scan time of 45 seconds. ROIs were placed automatically at the anterior cerebral artery for arterial input and superior sagittal sinus for venous outflow. Cerebral blood flow (CBF), cerebral blood volume (CBV), and mean transit time (MTT) maps were acquired by automatic calculation. All images were assessed independently by two radiologists (H.S. and Y.P.) with five years of experience in the evaluation of CTP for BD confirmation. Final decision was made by a consensus if there was a conflict in the results. Readers were blinded to the clinical examination and previous radiological reports in terms of BD diagnosis. CBV and CBF maps were evaluated qualitatively, and complete absence of perfusion in the cerebral parenchyma was accepted as cerebral circulatory arrest.

Statistical analysis

Statistical analysis was made using SPSS software version 21.0 (IBM). The Mann-Whitney U test was used to compare GM and WM density and the GM/WM density ratio of BD patients with the normal control group. Receiver operating characteristic (ROC) curves were analysed to identify the cut-off value of the GM/WM density ratio for the prediction of BD as well as calculating the sensitivity and specificity. Inter-rater variability was evaluated by using interclass correlation coefficient (ICC). r values including the range from 0 to 1.00 were described as follows: < 0.40, poor; 0.41-0.60, moderate; 0.61-0.80, good; ≥ 0.81, excellent agreement. A p value of less than 0.05 was considered statistically significant.

Results

Seventy-seven patients clinically diagnosed as BD (36 female, 41 male; mean age, 43.84 ± 23.25 years; range 0-80 years) and 77 age- and sex-matched control subjects (36 female, 41 male; mean age, 43.92 ± 23.07 years; range 0-80 years) were included. The mean GM/WM density ratio was 1.11 ± 0.12 (range, 0.78-1.33) in BD patients and 0.82 ± 0.07 (range, 0.68-1.02) in control subjects. The difference between groups was statistically significant (p < 0.001). The cut-off value for the GM/WM density ratio with the highest sensitivity and specificity was 1.07 (area under the ROC curve, 0.86; 95% confidence interval, 0.79-0.91). The sensitivity and specificity of the GM/WM density ratio were 83.6% and 89.6%, respectively. The inter-rater agreement for ROIs was evaluated by using ICC. The ICC values were 0.71 (95% confidence interval, 0.55-0.81) for GM, 0.72 (95% confidence interval, 0.56-0.81) for WM, and 0.70 (95% confidence interval, 0.54-0.81) for GM/WM density ratio.
0–83 years) were included in the study. The initial causes of coma were intracranial haemorrhage \((n = 36, 46.7\%)\), high-energy trauma \((n = 11, 14.2\%)\), cardiac arrest \((n = 10, 12.9\%)\), postoperative clinical conditions \((n = 8, 10.3\%)\), intoxication \((n = 6, 7.7\%)\), ischaemic stroke \((n = 3, 3.8\%)\), infection \((n = 2, 2.5\%)\), and asphyxia \((n = 1, 1.2\%)\).

In a comparison between the patient and control groups, WM and GM densities at the level of BG (caudate nucleus, putamen, corpus callosum, and posterior limb of internal capsule), CS, HC, BS (midbrain, pons, and medulla oblongata), and cerebellum were significantly lower in BD patients \((p = 0.019\) for HC–WM, \(p < 0.001\) for other areas). The GM/WM density ratio of CS, HC, and cerebellum were found to be significantly lower in BD patients \((p < 0.001\) for all levels), but there was no difference of GM/WM density ratio at the level of BG between the two groups \((p = 0.069)\) (Table 1).

ROC analysis of the GM/WM density ratio for predicting BD showed that the highest value of area under curve \((AUC)\) was found to be 0.907 at the level of HC \((AUC = 0.907, CI: 0.858–0.956)\). AUC values of CS, BG, and cerebellum level were identified as 0.837, 0.585, and 0.670, respectively (Figure 3). When a cut-off value of GM/WM density ratio at HC level was determined as 1.25, sensitivity and specificity values in predicting BD were 90% and 73%, respectively.

When CTP was assessed alone in patients with BD, 72/77 patients were interpreted as BD with sensitivity of 93%. The addition of CTP to the evaluation of the GM/WM density ratio of the HC level increased the sensitivity in predicting BD to 98% (Figure 4).

Inter-rater agreement of the radiologists in evaluating the density measurement of GM and WM from specified regions was found to be excellent at the level of BG for both GM and WM \((r = 0.869\) and 0.817, respectively); at the level of CS WM \((r = 0.894)\) and the level of HC WM \((r = 0.830)\). The lowest agreement was detected at the level of cerebellum WM, which was moderate \((r = 0.522)\). All values for each level are shown in Table 2.

### Discussion

In our study, the value of density measurement and the GM/WM density ratio in predicting BD were evaluated, and the GM-WM densities of each of 23 areas and the

### Table 1. Comparison of density values and ratio at each level between the patient and control groups

| Level                  | Patient group | Control group | \(p\)-value |
|------------------------|---------------|---------------|-------------|
| **Basal ganglia**      |               |               |             |
| BG grey matter         | 32.08 ± 4.27  | 42.05 ± 5.79  | < 0.001     |
| Caudate nucleus        | 31.46 ± 4.59  | 43.26 ± 6.90  | < 0.001     |
| Putamen                | 32.70 ± 4.60  | 40.84 ± 5.18  | < 0.001     |
| BG white matter        | 27.29 ± 3.11  | 35.26 ± 6.47  | < 0.001     |
| Corpus callosum        | 27.30 ± 3.32  | 36.09 ± 7.34  | < 0.001     |
| Posterior limb of internal capsule | 27.28 ± 3.71 | 34.42 ± 6.21  | < 0.001     |
| GM/WM density ratio    | 1.17 ± 0.12   | 1.20 ± 0.11   | 0.069       |
| **Centrum semiovale**  |               |               |             |
| Grey matter            | 33.26 ± 4.89  | 46.82 ± 9.17  | < 0.001     |
| White matter           | 29.33 ± 3.84  | 35.37 ± 7.36  | < 0.001     |
| GM/WM density ratio    | 1.13 ± 0.14   | 1.33 ± 0.14   | < 0.001     |
| **High convexity**     |               |               |             |
| Grey matter            | 35.67 ± 5.24  | 47.60 ± 9.82  | < 0.001     |
| White matter           | 32.60 ± 4.63  | 36.22 ± 8.21  | 0.019       |
| GM/WM density ratio    | 1.09 ± 0.11   | 1.32 ± 0.12   | < 0.001     |
| **Cerebellum**         |               |               |             |
| Grey matter            | 39.76 ± 7.57  | 49.98 ± 9.15  | < 0.001     |
| White matter           | 32.09 ± 5.28  | 37.01 ± 7.59  | < 0.001     |
| GM/WM density ratio    | 1.26 ± 0.31   | 1.36 ± 0.16   | < 0.001     |
| **Brainstem**          |               |               |             |
| Midbrain               | 30.54 ± 5.37  | 39.53 ± 9.14  | < 0.001     |
| Pons                   | 31.22 ± 6.29  | 36.80 ± 5.98  | < 0.001     |
| Medulla oblongata      | 27.82 ± 9.58  | 38.76 ± 6.70  | < 0.001     |

Data refer to mean value ± standard deviation. BG – basal ganglia, GM – grey matter, WM – white matter
GM/WM density ratio of each level except for BG were found to be significantly lower in BD patients compared to the control group (p = 0.019 for HC-WM, p < 0.001 for other areas). A cut-off value of GM/WM density ratio at the HC level was determined as 1.25 with a sensitivity of 90% and specificity of 73% for the prediction of BD. The sensitivity increased to 98% when CTP was used as an adjunct to density measurement.

Diffuse decrease in the cortical GM density has been defined as one of the CT findings of cerebral hypoperfusion [21]. This appearance could be explained by cytotoxic oedema, which occurs as a result of the disruption of the sodium-potassium pump in anoxic cells and is known to be more prominent in GM due to the high metabolic demand [21]. In our study, this finding was assessed by performing various HU measurements from brain parenchyma in brain-dead patients, and the GM density was found to be significantly low when compared to the control group at each level. Low density values in GM have also been shown in previous studies consisting of comatose or brain-dead patient groups [8,11,17,19]. However, there is a discrepancy between studies regarding the results of WM density. In many studies performed in comatose patients after cardiac arrest, WM values were not found to be statistically significant [14-17,22,23], whereas an increase in WM density compared to the control group was recorded in one study [11]. In our study, WM density was found to be significantly lower in patients with BD, which was also shown by Vigneron et al. [19]. This situation could be explained by the difference in characteristics of patient populations and possibly the timing of the CT scan.

Quantitative measurements on CT imaging have been commonly studied to evaluate the distinction of vegetative state-death or good-poor neurologic outcome after cardiac arrest [8,11,12,17,23,24]. The first study of the use of GM/WM density ratio to assess the prognosis of comatose patients after cardiac arrest was conducted by Torbey et al., in which the cut-off ratio was found to be 1.18 [11]. They indicated that values below this rate at the BG level were 100% predictive for death. In a meta-analysis involving 1150 patients from 10 studies, it was concluded that the GM/WM ratio had a high prognostic value in predicting a poor neurologic outcome in patients after cardiac arrest in the early period [25]. They reported that the cut-off values of seven studies at BG level were between 1.10 and 1.24 [25]. In a study consisting of 15 brain-dead patients conducted by Vigneron et al., the cut-off value was determined as 1.21 at basal ganglion level, but in their study the sensitivity was not stated [19]. In our study, with a greater patient population, it was found that values below 1.25 in the GM/WM ratio at the HC level could be useful in predicting BD with high sensitivity. Also, unlike in the above

Figure 3. Receiver operating curve analysis of grey matter/white matter density ratio at each level for predicting brain death

Figure 4. A 54-year-old female patient clinically diagnosed as brain death. A) Unenhanced axial computed tomography image at high convexity level shows diffuse cerebral edema and loss of differentiation between gray and white matter. The attenuation values of grey matter (GM) and white matter (WM) were 37 and 34 HU, respectively. GM/WM ratio was found as 1.08 which was below 1.25. (The regions where regions of interests are placed in gray and white matter were shown schematically with a white circle.) B) Cerebral blood volume map demonstrates the absence of cerebral perfusion which was compatible with brain death. (Cerebral blood flow and mean transit time maps not shown)
Utility of brain parenchyma density measurement and computed tomography perfusion imaging in predicting brain death

In our study, the density measurement at this level was found to have very close sensitivity values (90%) compared to CTP (93%) obtained in the same session. We suggest that measurements from this localisation could provide more reliable results in such a heterogeneous patient population with comorbid diseases and/or intracranial haemorrhage.

There are a number of studies that have investigated the contribution of CTP to CTA in confirmation of BD [2-4,26]. To our knowledge, this is the first study on evaluation of density measurements on unenhanced CT with the added value of CTP in predicting BD. According to the pattern of BD proposed by Palmer and Bader, a lack of cerebral blood flow is seen when intracranial pressure exceeds mean arterial pressure [1]. As a result, cerebral circulatory arrest leads to cytotoxic injury and subsequent irreversible neuronal damage. For determination of the absence of cerebral perfusion, CTP could be a suitable method in patients clinically diagnosed as BD. While the sensitivity of CTP was found to be 93% in our study, this value reached 98% with the addition of the GM/WM density ratio from the HC level. According to this result, we think that BD could be predicted with 98% sensitivity by performing a combined protocol of unenhanced CT scan and CTP with a 40 ml contrast media without CTA. However, this result needs to be supported by further studies involving more BD patients and a separate group of coma and intensive care patients as the control group.

Our study has several limitations. First, the timing of CT scan was not the same for all brain-dead patients. This condition might affect the attenuation of brain parenchyma among patients. However, in a study conducted by Metter et al., no significant relationship was found between the time from arrest to CT and the attenuation values in patients with cardiac arrest [8]. In another study, Scheel et al. reported that there was a gradual decrease in the median GM/WM density ratio value in CTs taken at six hours, 6-24 hours, and 24 hours, but there was no statistically significant difference between the three groups [23]. Contrarily, Wu et al. found a significant decrease in putamen density on CT taken at 24-72 hours compared to the first 24 hours [24]. However, as far as we know, there is no study on the alteration of attenuation over time after the diagnosis of BD. Second, in some patients, haematoma, herniation, shift, and artifacts passing through brainstem level caused difficulty in measuring the density. In order to determine the effect of this limitation on the results, interobserver reliability was evaluated and found to be in good or excellent agreement, except for cerebellum GM, midbrain, and pons levels, which is possibly due to the beam hardening artifacts passing through the posterior fossa. Third, CTP was performed after CTA because CTP has not yet been proven as a valid method in BD diagnosis. Contrast stasis in vessels may potentially create a limitation for the CTP. We attempted to minimise this limitation by allowing a waiting period of 10-15 minutes after CTA; a longer waiting period could not be performed because this patient group had to be followed under intensive care conditions.

Conclusions

The GM/WM density ratio at the HC level on unenhanced CT scan may be a useful finding to predict BD. The addition of CTP promotes this prediction by increasing the sensitivity. The combination of unenhanced CT and CTP might be reasonably acceptable by using lower amount of intravenous contrast media for BD patients who are potential candidates as donors for organ transplantation.

Conflict of interest

The authors report no conflict of interest.

Table 2. Inter-rater agreement results in evaluating the parenchymal density measurement

| Level            | Parenchymal density measurement | Reader 1 | Reader 2 | ICC (CI)          |
|------------------|---------------------------------|----------|----------|-------------------|
|                  |                                 | Mean ± SD | Mean ± SD |                  |
| BG-GM            |                                 | 32.13 ± 4.27 | 30.69 ± 3.67 | 0.869 (0.692-0.933) |
| BG-WM            |                                 | 27.29 ± 3.13 | 28.30 ± 3.17 | 0.817 (0.674-0.892) |
| CS-GM            |                                 | 33.26 ± 4.89 | 34.06 ± 4.70 | 0.737 (0.587-0.832) |
| CS-WM            |                                 | 29.33 ± 3.84 | 30.07 ± 3.57 | 0.894 (0.824-0.935) |
| HC-GM            |                                 | 35.67 ± 5.24 | 34.37 ± 4.58 | 0.808 (0.685-0.881) |
| HC-WM            |                                 | 32.60 ± 4.63 | 30.77 ± 4.02 | 0.830 (0.600-0.914) |
| Cerebellum-GM    |                                 | 39.76 ± 7.57 | 36.26 ± 4.50 | 0.522 (0.211-0.705) |
| Cerebellum-WM    |                                 | 32.09 ± 5.28 | 30.96 ± 3.56 | 0.669 (0.481-0.789) |
| Midbrain         |                                 | 30.55 ± 5.37 | 30.19 ± 4.58 | 0.738 (0.588-0.834) |
| Pons             |                                 | 31.22 ± 6.29 | 30.75±5.37 | 0.573 (0.325-0.729) |
| Medulla oblongata|                                 | 27.83 ± 9.58 | 30.45 ± 5.62 | 0.569 (0.323-0.726) |

Data of reader 1 and reader 2 refer to mean value ± standard deviation. CI – 95% confidence interval, ICC – interclass correlation coefficient, BG – basal ganglia, CS – centrum semiovale, HC – high convexity, GM – grey matter, WM – white matter.
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