Magnetic field sensor based on magnetoplasmonic crystal

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Here we report on designing a magnetic field sensor based on magnetoplasmonic crystal made of noble and ferromagnetic metals deposited on one-dimensional subwavelength grating. The experimental data demonstrate resonant transverse magneto-optical Kerr effect (TMOKE) at a narrow spectral region of 50 nm corresponding to the surface plasmon-polaritons excitation and maximum modulation of the reflected light intensity of 4.5% in a modulating magnetic field with the magnitude of 16 Oe. Dependences of TMOKE on external alternating current (AC) and direct current (DC) magnetic field demonstrate that it is a possibility to use the magnetoplasmonic crystal as a high-sensitive sensing probe. The achieved sensitivity to DC magnetic field is up to $10^{-6}$ Oe at local area of 1 mm².

Development of magnetic field sensors primarily works on improving the sensor’s design and its characteristics - sensitivity, resolution, locality and reliability as well as on extending the sensor’s operating temperature range or conditions of applicability (like harsh environments)1–4. One of the cutting-edge topics today is using the magnetic field sensors in medical applications such as magnetocardiography5,6 and magnetotomography7, which require precise measurements of magnetic field with the magnitude reaching 1 μOe. Nowadays the most reliable techniques are based on SQUIDs5,8, induction coil sensors9,10 and Hall-effect sensors11,12. These methods have several limitations connected with the decrease of sensitivity in small volumes13,14, the low temperatures requirement or moving the sensor probe for changing the sensing area. The alternative approach utilizes magneto-optical effects in transmission or reflection configurations, which allow one to preserve sensitivity at a local point and to scan the certain volume without moving the sensing element15–17. In this case the locality depends only on the optical beam size and the penetration depth of optical radiation in the medium, while the sensitivity is proportional to magnetization of the medium and the scanning volume can be changed by moving the optical spot.

One of the possible ways to increase the sensitivity of magneto-optical sensors is to get surface plasmon-polaritons (SPPs) excited on the metal-dielectric interface. SPPs induce the resonant magneto-optical effects appearing18–22. They increase the polarization plane rotation or modulation of the reflected (transmitted) light intensity utilizing the nonreciprocity of magneto-optical effects. The surface plasmons, being the electromagnetic excitations at the metal surface consisting of polaritons and electronic gas oscillations, require fulfilling the phase-matching conditions applying various experimental schemes, such as Kretchman, Otto and grating configurations23. Magneto-optical effects can be enhanced by SPPs in magnetoplasmonic crystals fabricated of noble metal and magnetic layers with one- or two-dimensional subwavelength grating20,24–27. There are several examples of using the magnetoplasmonic excitations in magneto-optical sensors of biomolecules15,28, chemical solutions29,30 and gases31 through detecting the ultralow refractive index changes32. Another promising direction is using the localized surface plasmons excited in metallic and hybrid nanoantennas17,33,34.

In this Letter, we show how the magnetoplasmonic crystal can operate as a highly sensitive local sensor of DC magnetic field. The use of controllable AC magnetic field allows one to choose the certain region at the magneto-optical response curve with the strongest dependence of the signal on the magnetic field magnitude. The sensor measures the DC magnetic field component parallel to the AC magnetic field while the shift of optical beam reveals the magnetic field distribution in the desired volume. The enhanced TMOKE, achieved due to excitation of SPPs, allows us to detect the magnetic field with sensitivity reaching $10^{-6}$ Oe.

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were obtained (Fig. 3a, solid red curve). The ratio of the magnetic moment modulation in fields with magnitude below 50 Oe36; (ii) the useful signal (relative magnitude of intensity changes on photodetector) on in magneto-optic measuring schemes for TMOKE is commonly more in comparison with LMOKE. For maximisation of the TMOKE signal measurements were carried out in the p-polarized light with the incidence angle fixed to $\Theta = 50^\circ$. The illuminated spot sizes were 12 mm$^2$ and 1 mm$^2$. Figure 1 shows the schematic view of the sensing element, the spatial profile of magnetoplasmonic crystals was passivated by a thin transparent layer of dielectric (silica nitride) to prevent oxidation of the iron layer. Thicknesses of functional layers were varied to estimate the contributions of magnetic and plasmonic properties into the enhancement of TMOKE and sensitivity of DC magnetic field sensor based on MPICs. The samples with thickness of iron layer above 50 nm can be considered as pure ferromagnetic gratings where magnetic contribution is dominant, while in the other samples the contribution of silver layer starts to play an important role in forming the magneto-optical response due to the increase of SPPs free mean path and extending the interaction of light with ferromagnetic material. The thickness parameters of functional layers of magnetoplasmonic crystals are listed in Table 1.

The surface profile and deposited layer thickness were examined by atomic force microscope (AFM) and scanning electron microscope (SEM), the magnetic properties were measured by vibrating sample magnetometer (VSM). Optical and magneto-optical properties were studied by a setup made up of the halogen lamp with a monochromator serving as a light source, Glan-Taylor prism as polarizer, a photomultiplier tube (model H10722-20 by Hamamatsu) with a lock-in amplifier as a detector accompanied by an optical chopper that controls the frequency of an optomechanical modulation or a system of electromagnets which allowed us to control the magnitudes of AC and DC magnetic field.

The setup schematics and the sample's design were optimal to be measured in TMOKE geometry according two reasons: (i) the magnetic field was applied in-plane along the easy magnetization axis, and gave the highest ratio of the magnetic moment modulation in fields with magnitude below 50 Oe; (ii) the useful signal (relative magnitude of intensity changes on photodetector) on in magneto-optic measuring schemes for TMOKE is commonly more in comparison with LMOKE. For maximisation of the TMOKE signal measurements were carried out in the p-polarized light with the incidence angle fixed to $\Theta = 5^\circ$. Frequencies of an optomechanical modulation or a system of electromagnets which allowed us to control the magnitudes of AC and DC magnetic field.

Table 1. Composition of magnetoplasmonic crystals.

| Sample number | Layer material (thickesses in nm) |
|---------------|-----------------------------------|
| Sample 1      | Ag(100)/Fe(100)/Si$_3$N$_4$(20)  |
| Sample 2      | Ag(100)/Fe(50)/Si$_3$N$_4$(20)  |
| Sample 3      | Ag(100)/Fe(20)/Si$_3$N$_4$(20)  |
| Sample 4      | Ag(100)/Fe(5)/Si$_3$N$_4$(20)   |

Results and Discussions

Sample characteristics and geometry. Magnetoplasmonic crystals were fabricated by ion-beam deposition of noble (silver) and ferromagnetic (iron) metal layers onto the surface with quasi-sinusoidal subwavelength polymeric grating. Before the fabrication the chamber was vacuumed down to 8 $\times$ 10$^{-7}$ Torr. During the fabrication process the argon flow of 6 ccm and ion source MPC-3000HC with working current of 30 mA and voltage of 1000 V were used. All the substrates were rotating during the fabrication process to avoid the shadowing effect. The period and profile height of the grating were equal to 320 and 20 nm, respectively$^{35,36}$. Surface of magnetoplasmonic crystals was passivated by a thin transparent layer of dielectric (silica nitride) to prevent light-matter interaction and results into the resonant enhancement of TMOKE and sensitivity of DC magnetic field sensor based on MPICs. In the case of thickness of iron layer above 50 nm the samples can be considered as pure ferromagnetic gratings where magnetic contribution is dominant, while in the other samples the contribution of silver layer starts to play an important role in forming the magneto-optical response due to the increase of SPPs free mean path and extending the interaction of light with ferromagnetic material.

Experimental demonstration. The TMOKE value is defined as $\delta = (R_{\perp H} + R_{\parallel H})/R_0$, where $R_0$ is the reflection amplitude without magnetic field, which was detected with optomechanical modulation of the incident light, $R_{\perp H}$ and $R_{\parallel H}$ denote the field dependent reflection amplitudes. Measurements of spectral dependencies of reflectivity and TMOKE were carried out in saturation AC magnetic field of 50 Oe. Reflection and TMOKE spectra for Sample 1 are shown in Fig. 1d.

The minimum of the specular reflectivity and the maximum of the TMOKE signal are clearly observed at the resonant wavelength of 618 nm and related to strong coupling of plasmon oscillations and the light diffracted into the -1st order$^{37}$. The excited SPPs tightly localize the electric field of the incident electromagnetic wave at the Fe/Si$_3$N$_4$ interface that leads to efficient light-matter interaction and results into the resonant enhancement of TMOKE.

Figure 2a shows the set of minor hysteresis loops measured by VSM from the saturation magnetic field of $H_{sat} = 50$ Oe: the field magnitude was gradually decreased by a small step value of $H_{step}$, where $H_{step}$ is a step number. By this way the sample was demagnetized and values of $\Delta M(H_{sat}) = M(+H_{sat}) - M(-H_{sat})$ were obtained (Fig. 3a, solid red curve). The $\Delta H$ value shown by dashed lines corresponds to the region of rapidly decreasing $\Delta M(H)$ and denotes the field region of hysteresis loop collapse.

The noise of the sensor prototype is measured at the resonant wavelength and saturation magnetic field as the time dependence of PMT voltage output for 500 points with 3 seconds per point. Then, the standard deviation $\sigma = \sqrt{(x_N - \bar{x})^2/(N - 1)}$, where $N$ is a number of acquisition points, is used to calculate the signal-to-noise ratio $SNR_{AC} = (R_{\perp H} - R_{\parallel H})/\sigma$, where $(R_{\perp H} - R_{\parallel H})$ value were accumulated for 3 seconds at a given magnetic field and sensitivity $\Delta SNR/\Delta H$, where $\Delta SNR$ is the difference of maximum and minimum $SNR$ values in selected $\Delta H$ range.

Figure 2b shows the dependences of the signal-to-noise ratio $SNR_{AC}$ on AC magnetic field for all samples. The $SNR_{AC}$ dependences have a step-like behaviour: in AC magnetic field with an amplitude of the saturation field, $SNR_{AC}$ has the maximum value and starts to decrease to zero with decrease of the magnetic field. The width of...
the step for the Sample 1 is $\Delta H = 2.8$ Oe and shown by the dashed lines which corresponds the field region of hysteresis loop collapse shown in Fig. 2a.

The $SNR(H_{DC})$ dependence was obtained by (i) setting of $H_{AC}$ value to the maximum of the derivative $\frac{\partial SNR_{AC}}{\partial H_{AC}}$ that allows one to get the point in the center of the observed slope of $SNR(H_{AC})$ dependence and (ii) application of additional magnetic field $H_{DC}$ with the magnitude of $\pm 0.18$ Oe. This way $SNR(H_{DC})$ was measured for all samples and compared with the relative changes of iron layer magnetic moment $\Delta M$ obtained by demagnetizing the sample using VSM. The shape of magneto-optical response dependence on magnetic field correlates with the relative changes in magnetic moment of iron layer which can be written as $\delta = (R_{+H} + R_{-H})/R_0 \sim \Delta M = M_{+H} - M_{-H}$. Typical dependences of $SNR(H_{AC}), SNR(H_{DC})$ and $\Delta M(H)$ are presented in Fig. 3a.

$SNR_{AC}$ and $SNR_{DC}$ dependences show that the magneto-optical response depends on a sum of magnitudes of AC and DC magnetic fields affecting the magnetoplasmonic crystal in the direction perpendicular to the plane of light incidence and proportional to a magnetic moment of ferromagnetic layer. It is possible to use the $SNR_{DC}$
dependence as a calibration curve for estimating the reliable and precise correlation between the field dependent magneto-optical response and the external field magnitude.

Two functions are considered to reveal the dependence of magnetic field sensors sensitivity on the iron layer thickness in magnetoplasmonic crystals. The first one, $\delta/\Delta H$, is shown in Fig. 3b and depends both on the maximum modulation of optical reflectance by magnetic field at the wavelengths corresponding to excitation of SPPs and on the width of the step in $SNR_{AC}$ dependence. The second dependence, $Max(SNR_{AC})$, describes the dependence of $SNR_{AC}$ at saturation magnetic field on the thickness of the iron layer in magnetoplasmonic crystals. Variation of the iron layer thickness allows one to tune the sensitivity by changing optical and magnetic properties of magnetoplasmonic crystals. Magnetic moment and optical losses monotonously increase with the iron layer thickness, while the shape of $\delta/\Delta H$ dependence is mostly determined by non-monotonic changes of the coercive force and $\Delta H$ value. The shape of $Max(SNR_{AC})$ strongly depends on the iron layer magnetization and monotonously increases with the growing iron layer thickness. The sensitivities of DC magnetic field sensor prototypes based on magnetoplasmonic crystals are estimated to be $3.7 \times 10^{-6}$, $3.2 \times 10^{-5}$, $3.4 \times 10^{-5}$ and $3.8 \times 10^{-5}$ Oe at a room temperature for iron layer thickness of 100, 50, 20 and 5 nm, respectively. Thus, it is shown that sensing capabilities are stronger correlated with the value of magnetic moment, than with the plasmonic properties and value of optical losses. The highest sensitivity is achieved for the sample with the iron layer thickness of 100 nm.

Further increase of the TMOKE value is achieved by optimizing the illuminated spot size. For Sample 1 the $SNR_{AC}$ value at saturation magnetic field is changed from $2.7 \times 10^6$ to $3.2 \times 10^5$ with decreasing the spot size from 12 mm$^2$ to 1 mm$^2$ due to the difference in magnetization processes: using a small region in the center of magnetoplasmonic crystal allows one to increase the steepness of the magnetization curve by neglecting the edge effects which lead to domain nucleation with opposite magnetization direction in lower magnetic field. With the decrease of the spot size the value of sensitivity changes from $3.7 \times 10^{-6}$ to $3.1 \times 10^{-6}$. The minimal optical spot size to use the magnetoplasmonic crystal as a magnetic field sensor is determined by the following parameters: diffraction limit, wavelength of SPPs excitation and fulfilling the diffraction conditions and is estimated to be as small as 5 $\mu$m$^2$. The theoretical limit of sensitivity of $10^{-7}$ Oe is estimated as a sum of four noise sources, namely, thermal $i_{th} = \sqrt{4kT R \Delta f}$, flicker $i_{fl} = 1/f^{1/2}$, shot $i_{sh} = \sqrt{(2qI/2\pi)}$, and avalanche $i_{av} = \sqrt{(2qI/2\pi)}$ noises and did not exceed the value of $6 \times 10^{-7}$ that was by two orders smaller than the measured noise value. Table 2 compares the sensitivity and locality of various magnetic field sensors and reveals the advantages of the designed sensing element. The sensor based on magnetoplasmonic crystal as a probe provides high sensitivity at small spot size which makes it sufficient and promising for biomedical applications and allows one to scan the surface area without moving the probe element.

**Figure 3.** Panel (a) shows the magnetic field dependences of SNR and $\Delta M$ for the Sample 1. Blue dashed lines show DC magnetic field range. Inset zooms the central part of the SNR dependence. Panel (b) shows dependences of $\delta/\Delta H$ and $Max(SNR_{AC})$ values on iron layer thickness.

| Magnetic field sensor type | Hall effect$^{12,37,38}$ | Magneto-modulation$^{9,13,39,40}$ | Magneto-optical$^{15,41}$ | Magnons$^{42}$ | Magnetoplasmonic Prototype | Theory |
|---------------------------|---------------------------|-----------------------------|------------------------|-------------|---------------------------|--------|
| Sensitivity               | $10^{-6}$ Oe              | $10^{-7}$ Oe                 | $10^{-5}$ Oe           | $10^{-2}$ Oe | $3 \times 10^{-6}$ Oe     | $10^{-7}$ Oe |
| Probe Size                | 200 nm$^2$                | 1 mm$^2$                    | 5 $\mu$m$^2$           | 4-9 cm$^2$ | 1 mm$^2$                  | 5 $\mu$m$^2$ |

**Table 2.** Comparison of sensors in terms of the probe sensitivity and locality.
Conclusions

Summarizing, here we demonstrate DC magnetic field sensors based on magnetoplasmonic crystals made of noble and ferromagnetic metals deposited on one-dimensional subwavelength grating utilizing TMOKE enhanced by excitation of SPPs. The correlation between magnetic optical and magnetic properties reveals the possibility to tune the sensitivity of the sensor by changing the ferromagnetic layer thickness. The sensitivity of the sensor prototype based on the magnetoplasmonic crystal was found to be 3 · 10⁻⁶ Oe with the spot size of 1 mm² and can be further improved by optimizing the sensing element and the sensor's setup overall design.

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References

1. Tumanski, S. Modern magnetic field sensors - a review. Prz. Elektrotech. 89(10), 1 (2013).
2. Zhai, J., Xing, Z., Dong, S., Li, J. & Viehland, D. Detection of pico-Tesla magnetic fields using magneto-electric sensors at room temperature. Appl. Phys. Lett. 88, 062510 (2006).
3. Stutze, N. A., Russek, S. E., Pappas, D. P. & Tondra, M. Low-frequency noise measurements on commercial magnetoresistive sensors. J. Appl. Phys. 97, 10Q107 (2005).
4. Budker, D. & Romalis, M. Optical magnetometry. Nat. Physics 3, 227 (2007).
5. Tsukada, K. et al. Multichannel SQUID system detecting tangential components of the cardiac magnetic field. Rev. Sci. Instrum. 66, 5085 (1995).
6. Koch, H. Recent advances in magnetocardiography. J. Electrocardiol. 37, 117 (2004).
7. Marmugi, L. & Renzoni, F. Optical magnetic induction tomography of the heart. Sci. Rep. 6, 23962 (2016).
8. Drung, D. et al. Highly sensitive and easy-to-use SQUID sensors. IEEE Trans. Appl. Supercond. 17, 699 (2007).
9. Tumanski, S. Induction coil sensors: A review. Meas. Sci. Technol. 18, R31 (2007).
10. Deans, C., Marmugi, L., Hussain, S. & Renzoni, F. Electromagnetic induction imaging with a radio-frequency atomic magnetometer. Appl. Phys. Lett. 108, 103503 (2016).
11. Michele, L. et al. Detection and susceptibility measurements of a single Dykn bead. J. Appl. Phys. 110, 063916 (2011).
12. Sandhu, A., Okamoto, A., Shibasaki, I. & Oral, A. Nano and micro Hall-effect sensors for room-temperature scanning hall probe microscopy. Microelectron. Eng. 73-74, 524 (2004).
13. Ripka, P. & Janosek, M. Advances in magnetic field sensors. IEEE Sens. J. 10, 1108 (2010).
14. Grigorashvili, Yu, E. L. & Volik, N. N. Magnetomodulation sensor of a weak magnetic field based on HTS (Bi, Pb)2Sr2Ca2Cu3Ox ceramics. Physica C 435, 140 (2006).
15. Sepulveda, B., Calle, A., Lechuga, L. M. & Armelles, G. Highly sensitive detection of biomolecules with the magneto-optic surface-plasmon-resonance sensor. Opt. Lett. 31, 1085 (2006).
16. Inoue, M. et al. Investigating the use of magnonic crystals as extremely sensitive magnetic field sensors at room temperature. Appl. Phys. Lett. 98, 133511 (2011).
17. Maccafferri, N. et al. Ultrasonic and label-free molecular-level detection enabled by light phase control in magnetoplasmonic nanofanels. Nat. Commun. 6, 6150 (2015).
18. Krinchik, G. S., Chepurova, E. E. & Kraeva, T. I. Excitation of magnetized-plasma surface-waves in nickel. JETP Lett. 40, 776 (1984).
19. Clavero, C., Yang, K., Skaza, J. R. & Lukashev, R. A. Magnetic field modulation of intense surface plasmon polaritons. Opt. Express. 18, 7743 (2010).
20. Grunin, A. A., Zhdanov, A. G., Ezov, A. A., Ganshina, E. A. & Fedyanin, A. A. Surface-plasmon-induced enhancement of magneto-optical Kerr effect in all-nickel subwavelength nanogratings. Appl. Phys. Lett. 97, 261908 (2010).
21. Chetvertukhin, A. V. et al. Magneto-optical Kerr effect enhancement at the Woods anomaly in magnetoplasmonic crystals. J. Magn. Magn. Mater. 324, 3516 (2012).
22. Belotelov, V. I. et al. Plasmon-mediated magneto-optical transparency. Nat. Commun. 4, 2128 (2013).
23. Zayats, A. & Smolyaninov, I. Near-field photonics: surface plasmon polaritons and localized surface plasmons. J. Opt. A: Pure Appl. Opt. 5, S16 (2003).
24. Belotelov, V. I. et al. Enhanced magneto-optical effects in magnetoplasmonic crystals. Nat. Nanotechnol. 6, 370 (2011).
25. Shcherbakov, M. R., Vasilievich, P. P., Frolov, A. Y., Dolgova., T. V. & Fedyanin, A. A. Femitosecond intrapulse evolution of the magneto-optic Kerr effect in magnetoplasmonic crystals. Phys. Rev. B 90, 201409(R) (2014).
41. Koschny, M. & Lindner, M. Magneto-optical sensors accurately analyze magnetic field distribution of magnetic materials. *Adv. Mat. and Proc.* 2, 13 (2012).

42. Valente, J. A magneto-electro-optical effect in a plasmonic nanowire material. *Nat. Commun.* 6, 7021 (2015).

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**Author contributions**

V.V.R. and V.K.B. conceived magnetic experiments. A.A.G. and A.A.F. conceived the optical experiment. V.K.B. conducted all the experiments. M.I. provided deposition and characterisation equipment and assisted with fabrication of samples. All authors took part in analysing the results and reviewed the manuscript.

**Competing interests**

The authors declare no competing interests.

**Additional information**

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