Abstract. Plasma medicine comprises the application of physical plasma directly on or in the human body for therapeutic purposes. Three most important basic plasma effects are relevant for medical applications: i) inactivation of a broad spectrum of microorganisms, including multidrug-resistant pathogens, ii) stimulation of cell proliferation and angiogenesis with lower plasma treatment intensity, and iii) inactivation of cells by initialization of cell death with higher plasma treatment intensity, above all in cancer cells. Based on own published results as well as on monitoring of relevant literature the aim of this topical review is to summarize the state of the art in plasma medicine and connect it to redox biology. One of the most important results of basic research in plasma medicine is the insight that biological plasma effects are mainly mediated via reactive oxygen and nitrogen species influencing cellular redox-regulated processes. Plasma medicine can be considered a field of applied redox biology.

Plasma medicine is a new field of research combining plasma physics, life science and clinical medicine. Basically, medical application of physical plasma comprises two principal approaches: i) use of plasma-based or plasma-supplemented techniques to treat surfaces, materials or devices to realize specific qualities for subsequent special medical applications, and ii) direct application of physical plasma on or in the human (or animal) body to apply therapeutic effects based on direct interaction of plasma with living tissue. Plasma application for the treatment of medical materials or devices is an important subject of research and has been utilized for several years now (1-8). However, the core area of plasma medicine – as a new field of research – focuses on the use of plasma technology in direct treatment of living cells and tissues. The aim of applied plasma medicine is to exploit a differentiated interaction of specific plasma components with specific structural, as well as functional elements or functionalities of living cells to control, and ideally, normalize therapeutic effects. Besides its antimicrobial activity, exposure of mammalian cells to physical plasma can lead either to stimulation or inhibition of cellular function (9). Consequently, most research and primary medical application of physical plasma is concentrated on wound healing and cancer treatment. During recent years, a broad spectrum of different plasma sources (called by many different names and abbreviations) has been designed and dedicated for biomedical applications (9-12).

Plasma Generation and Plasma Sources for Biomedical Applications

Physical plasma is a special excited gas state, sometimes named “the fourth state of matter” following solid, liquid, and gaseous states. It can be generated by a continuous supply of energy to the atoms or molecules of a neutral gas until an excited state is achieved. The energy required may be provided separately by thermal, chemical, electrical and radiative resources or a combination of all. However, the predominant ionizing mechanism is the collision process that involves inelastic collision, electron impact, radiative interactions and charge exchange. As the typical life span of excited states is about 10 ns stopping the energy supply starts a depletion process rapidly quenching the plasma. The electron impact ionization is the most robust procedure generating a plasma for biomedical purposes. The energy is transferred by inelastic and elastic collisions of high-energy
electrons generated by a strong electric field with the atoms or molecules in the gas resulting in its partial ionization. The temperature of such partially ionized gas is always substantially lower than the characteristic ionization temperature. In a well-designed plasma source, ambient temperature of the plasma can be achieved. The physicochemical characteristics of plasma can be complex and they depend on a multitude of parameters, including the type and composition of the gas or gas mixture used for plasma generation, the applied energy and electrode configuration, the pressure, and the environment. Consequently, a broad range of parameters can be controlled by the plasma source design. With regard to its application, especially in the medical context, useful classifications are thermal versus non-thermal plasmas and low pressure versus atmospheric pressure plasmas (13-15). For a direct application on living tissue as the main aim of plasma medicine, only plasma generated under atmospheric conditions should be used. Medical treatment techniques using such plasmas have been firmly established for a long time in the field of electro surgery, even if they were not explicitly referred to as plasma medicine at the time. Such techniques, like argon plasma coagulation (APC), rely on precisely targeted thermal necrotization of tissue to achieve hemostasis (cauterization), or to cut or remove tissue (16, 17). Furthermore, several plasma-based devices in cosmetics, e.g. for wrinkle removal and skin regeneration, also rely on thermal plasma effects (18, 19). Since the 1990s, technologies for stable and reproducible plasma generation at low temperature under atmospheric conditions are available on a larger scale, facilitating the generation of so-called cold atmospheric plasmas (CAP). This has led to considerable intensification of research in the field of medical applications of physical plasma at tissue-compatible temperatures. In terms of medical application, “cold” means temperatures lower than 40°C at the target site during plasma treatment (9).

Simplifying, generation of CAP and its components can be summarized with the following three steps (9, 11, 14):

i) Ionization and excitation of atoms or molecules of a neutral gas (argon, helium, oxygen, nitrogen, air, or mixtures thereof) via electron impact by supplying electrical energy;

ii) Interaction of electrons and high energy states of atoms or molecules with reaction partners in the plasma phase and its vicinity (ambient air, liquids, surfaces), generating secondary and tertiary reactive species;

iii) Emission of electromagnetic radiation (UV, visible light, IR/heat, electric fields) formed by excitation and depletion processes or charge transport.

It is important to note that the plasma state is maintained as long as the energy supply exists, i.e. it is not possible to store a plasma like a gas.

Because plasma contains highly motile electrons it is conductive and can transfer electrical current to cells and tissue with possible biological consequences (20). Also, the emitted electromagnetic radiation, above all the ultraviolet (UV) light, has the potential to elicit biological effects (21, 22). However, according to the current state of knowledge, free electrons, high energy states of atoms and molecules along with ions and radicals in the plasma and those generated in secondary reactions are the main components of the chemical reactivity and biological activity of a plasma (23). The sum of the CAP derived chemical entities is often circumscribed as reactive species.

A large number of plasma sources that are potentially useful for medical applications are described in the literature. They differ in their plasma generation mechanism, source geometry, working gases, and, consequently, vary in their application characteristics (9, 12, 24-28). During recent years, mainly two fundamental concepts of CAP devices have been tested and are partially applied for medical purposes: i) dielectric barrier discharges (DBD) and ii) plasma jets (9, 29-32).

In Figure 1, three technical principles of plasma sources intended for biomedical applications are depicted (11, 30).

The volume DBD (Figure 1A) is characterized by plasma ignition in a gap between an isolated high voltage electrode and the target to be treated. Consequently, cultured cells or living tissues in biomedical application are part of the discharge electrode configuration. Plasma has a direct contact with the target to be treated and the target is directly exposed to the electrical field that is necessary for plasma generation (9, 31). In the surface DBD (Figure 1B), plasma is ignited around an individually designed electrode structure (e.g. circular or grid-like), which is isolated from a counter electrode. There is no direct contact of the active plasma with the target to be treated, instead impact is achieved by transport processes bringing the reactive species to the living tissue. With both DBD configurations, atmospheric air usually serves as the working gas for plasma generation. Both volume and surface DBD devices are suitable to generate plasmas over larger areas (9, 31). In a plasma jet device (Figure 1C), the electrode setup for plasma generation is located in or around a tube-like arrangement, in most cases inside a pen-like device. Diverse electrode configurations can be used, e.g. pin electrodes, ring electrodes, plate electrodes etc. The plasma is ignited inside the device using a working gas that is flowing through the tube. The so-called plasma effluent (or afterglow) is carried out along the gas flow and can be brought into direct contact with the target to be treated. In order to maintain a low temperature and to achieve excellent controllability of the discharge, most plasma jet devices are using noble gases (helium or argon) as working gas, often doped with small amounts of molecular gases (nitrogen, oxygen). The target to be treated is not part of the electrode configuration. However, because of the conductivity of the plasma and its afterglow, small
electrical currents may pass to the target. By choosing an appropriate design of electrode and high voltage waveform these currents can be easily controlled (9, 29, 32).

One of the best-investigated plasma sources for biomedical application is the argon-driven cold atmospheric pressure plasma jet, kINPen (Figure 1C) (32-34). A needle electrode inside a dielectric capillary is powered with a sinusoidal high voltage (2-6 kVpp) with a frequency of 1.0-1.1 MHz (power <3.5W in the hand-held unit). Argon gas with a flow rate of 3-5 standard liters per minute (slm) is used as the working gas. The plasma is generated at the tip of the needle and is subsequently released with the feed gas flow into the atmospheric environment, thereby generating a typical plasma effluent with a length of 9-12 mm and with 1 mm in diameter. Under these conditions, the electron density in the core plasma region near the high voltage electrode tip is in the order of $10^{12}$ cm$^{-1}$ and one order of magnitude lower in the visible effluent zone. However, electron density depends on several parameters and can be varied by admixture of molecular gases, such as oxygen and nitrogen (32).

The reactive species generated inside the plasma or as a result of plasma interactions with the surrounding media are considered the most important components responsible for biological plasma effects. In the kINPen, the argon-based plasma effluent is exposed to atmospheric air containing predominantly oxygen, nitrogen, and water. Traces of these, especially oxygen, are contained in the working gas in low ppm-amounts, too. These atmospheric air compounds are the precursors for secondarily generated non-radical and radical reactive oxygen and nitrogen species (ROS, RNS). Generation of ROS and RNS can also be modulated by controlled admixture of oxygen, nitrogen, water or air to the argon working gas flow, or by gas shielding and modification of the atmosphere around the plasma effluent (32). When the effluent containing the ROS, RNS, and residual high energy states targets a liquid (a tissue), a number of transport processes and tertiary reactions with target molecules occurring is so far not fully understood. Current knowledge assumes that at the interface between gas phase and liquid (or solid) target as well as in the target bulk a considerable rearrangement of the ROS/RNS pattern occurs (Figure 2) (32, 35-38). Beside an interaction of the plasma derived species among themselves, the interaction with target biomolecules results in the formation of diverse chemical structures acting as a messenger or a beacon.

Because all plasma sources for biomedical applications are working under atmospheric air conditions or use ambient air as working gas, the generation of ROS and RNS from air-based oxygen and nitrogen is a corresponding feature of all these plasma sources. However, the composition and quantity of plasma-generated ROS and RNS, as well as UV irradiance, electrical field and other characteristics, are strongly dependent on specific plasma sources and device parameters as working gas composition, power input and temperature (39).

Biological Plasma Effects and its Medical Use: Focus on Wound Healing

Among the vast number of experimental reports on biological plasma effects (using different plasma sources and devices under varying conditions), three effects most important for a medical application are consistently reported (30):

i) Effective inactivation of a broad spectrum of microorganisms including multidrug-resistant pathogens;

ii) Stimulation of cell proliferation and angiogenesis with lower plasma treatment intensity and time;

iii) Initialization of (programmed) cell death with higher plasma treatment intensity and time, primarily in cancer cells.

With the improved availability of CAP technology in the 1990s, its antimicrobial activity was in the early focus of research with regard to microbial decontamination or sterilization of materials and devices (40, 41). Extensive
research has been done on the mechanisms of low-pressure cold plasma interaction with microorganisms. This was mainly attributed to UV-based DNA damage in combination with erosion of microorganism structures by UV-based photodesorption and etching processes by reactive plasma species (42-45). However, the knowledge on mechanisms of inactivation of microorganisms by CAP is limited. Microbicidal CAP effects are mainly attributed to the activity of ROS and RNS leading to oxidative damage and modification of cytoplasmatic membrane, proteins, and DNA (46-48). Furthermore, induction of apoptosis-like processes of programmed cell death in bacteria is being discussed as a potential mechanism (49). Other physical mechanisms are currently under investigation, for instance electrostatic disruption by plasma-derived charged particles, or electroporation caused by plasma-related electric fields (49, 50).

Regardless of the specific mode of action, early experimental evidence on microbicidal plasma effects on heat or radiation-sensitive material surfaces spurred further efforts to investigate plasma effects on contaminated or infected tissue. Several in vitro studies on effective inactivation of clinically relevant microorganisms and viruses have produced promising results (51-58). The first clinical investigations on antiseptic plasma effects on tissue and wounds that followed have shown rather modest microbial reduction rates (59-63). However, improvement of wound healing in general has been partially seen during these clinical investigations (61, 64). Some additional case reports and clinical investigations with different plasma devices support these findings (65, 66).

Starting in 2013, the first cold atmospheric pressure plasma devices received CE certification as medical devices for the purpose of treating chronic wounds as well as pathogen-based skin diseases in Germany and Europe. These include the argon-driven, jet-like CAP devices kINPen MED (neoplas tools GmbH Greifswald, Germany) and SteriPlas (ADTEC, Hunslow, UK) as well as the DBD-based devices PlasmaDerm (CINOGY GmbH Duderstadt, Germany) and plasma care (terraplasma medical GmbH Garching, Germany), the latter two using atmospheric air as working gas. Certification of all these devices was based on comprehensive physical and biological characterization of the respective plasma source accompanied with clinical investigations (9, 10, 25, 34, 53, 55, 59-64). However, even if randomized controlled clinical trials are not available as yet (as unfortunately is the case for many wound therapies due to a lack of standardization in wound scoring), positive experiences are consistently reported from the medical practice. Particularly in chronic wounds, e.g. venous leg ulcers where any conventional therapeutic options have been exhausted, a clear benefit of CAP treatment has been found. Some practitioners have reported a re-start or acceleration of wound healing process in more than 80% of cases as a preliminary result, particularly following the use of the kINPen MED (11, 30). Now, the most important aim is to validate these results by systematic clinical data.

These clinical experiences confirm a very early hypothesis in plasma medicine research, that plasma effects on wound healing may be a result of a two-step activity: antiseptics on wound surface in combination with stimulation of tissue regeneration (67). Several experimental in vitro studies could demonstrate a direct impact of CAP on cell proliferation and migration as well as on angiogenesis (68-76). The stimulating effect on skin tissue regeneration was confirmed.
in several in vivo animal experiments (69, 74-90) and in human volunteers or patients with reasonably defined wounds (91-93). It has to be pointed out that these last-mentioned wound healing effects in vivo were demonstrated in acute wounds without any interfering microbial contamination. With plasma treatment, the spontaneous wound healing process was not impeded, and there was an acceleration in the early stage of wound healing. With this direct proof of stimulation of wound healing by plasma treatment, it seems that the antiseptic plasma effect can be partially pushed into the background because it may turn out that it is not the dominating process as it was assumed for several years. Consequently, as a next step in clinical research, it should be investigated, if this early stimulation of wound healing may have any beneficial effects also in acute wounds, e.g. with regard to scar formation or prevention of complications in wound healing. Possible fields of application of CAP in acute wound healing could be in patients with co-morbidities leading to a high risk of disturbed wound healing and subsequent chronification, in the case of large-area burns or in the treatment of skin graft donor and acceptor sites (92, 94).

Nevertheless, there should be no doubt that plasma-induced antiseptics have an important additional effect in the case of contaminated wounds. Here, a very important question is why plasma is destructive or inactivating for microorganisms while stimulating repair mechanisms on mammalian cells. There is some evidence that the ROS-RNS composition resulting from plasma generation under atmospheric air conditions is more toxic for microorganisms because both oxygen- and nitrogen-containing reactive species are required for antimicrobial effects, whereas mammalian cell toxicity is mostly dependent on oxygen-based reactive species (95). Another very interesting insight is that, because of the role of ROS generated by immune cells to fight wound infection, wounded tissue takes cytoprotective measures to promote some tissue “resilience” for protection against ROS caused damage (96). This physiological mechanism may also be protective against plasma-generated ROS and RNS.

**Redox Biology as the Scientific Grounding of Plasma Medicine**

The fact that the biological effects of CAPs are mainly based on ROS and RNS, was primarily reasoned from experimental observations in vitro. Plasma effects on mammalian cells were found to be dependent on cell culture media composition, each exhibiting a different antioxidative potential. Additionally, biological plasma effects could be extinguished when antioxidants like N-Acetylcystein (NAC) were added (97-99). A multitude of investigations on plasma-liquid interactions has demonstrated the occurrence of ROS and RNS in liquid phases following plasma treatment (36, 37). Moreover, it has been shown several times that liquids, such as water, physiological saline, or cell culture media become biologically effective following plasma treatment (100-105). This underlines a key role of liquid phase composition for biological plasma effects. ROS and RNS like superoxide (O$_2^-$•), hydrogen peroxide (H$_2$O$_2$), hydroxyl radical (•OH), singlet oxygen (1O$_2$), ozone (O$_3$), and RNS, such as nitric oxide (•NO), nitrogen dioxide (•NO$_2$) and peroxynitrite (ONOO-), are transferred from plasma into the liquid environment of cells and tissue, or they are generated by a very complex network of secondary liquid reactions (Figure 2) (23, 106-111).

This insight of the central role of ROS and RNS has opened up the door to the field of redox biology to explain and interpret biological effects caused by CAP. Redox biology can be taken as the interface between the more or less unspecific impact of external factors and the specific response and adaptation of a cell or an organism via its metabolic and macromolecular structures (112). Meanwhile, it is well known that ROS and RNS are not solely harmful in cells, but also serve as signaling molecules via reversible oxidations and reductions of specific protein structures with cysteine as a major reaction target (113). In a comprehensive in vitro study using different jet-based plasma devices with different working gas mixtures, the cysteine-oriented plasma chemistry could be proven. Furthermore, it could be demonstrated that cysteine is a useful and sensitive tracer compound to discriminate between the chemical potential of different plasma sources or gas mixtures, respectively (114).

One of the most important players for ROS and RNS-based regulation in cell physiology is the mammalian Kelch-like ECH-associated protein 1 (Keap1)-nuclear factor erythroid 2-related factor (Nrf2) pathway. In regular cell physiology, it uses cysteine oxidation to respond to increased ROS levels. By redox modification of cysteine-residues of Keap1, Nrf2 is released from its complex and the E3 ubiquitin ligase cullin 3 (CUL3). Subsequently, Nrf2 translocates from the cytosol to the nucleus where it binds to antioxidant responsive elements (ARE) on DNA, promoting the upregulation of antioxidant genes (113, 115). It has been demonstrated that CAP treatment of human keratinocytes in vitro leads to the stimulation of this Nrf2 pathway, resulting in the translocation of Nrf2 into the nucleus and the subsequent activation of Nrf2-ARE-targets, such as glutathione (GSH), glutathione reductase (GSR), glutathione S-transferase (GST), superoxide dismutase (SOD), heme oxygenase 1 (HMOX-1), and NADPH quinine oxidoreductase 1 (NQO1) (90, 116). Moreover, in an acute wound healing study in mice, an early activation of the Nrf2 pathway has also been demonstrated in vivo and ex vivo on skin tissue, dermal fibroblasts and epidermal keratinocytes (Figure 3) (76, 117).
This Nrf2 pathway stimulation by CAP treatment seems to be one of the most important mechanisms to protect mammalian cells from genotoxic plasma effects. Indeed, a huge number of in vitro studies report on potential genotoxic CAP effects on isolated, naked, or cellular DNA (118). However, several investigations of potential genotoxic effects of CAP by in vitro standard procedures for mutagenicity testing of chemical substances has demonstrated no extended mutation rate of plasma treated cells (119-123). The main conclusion is that CAP treatment causes no enhanced genotoxic risk. This has also been confirmed in an animal study using hairless immunocompetent mice (124), in CAP-treated skin biopsies (125-127), and in clinical follow-up investigations of plasma-treated wounds (128, 129).

Meanwhile, it is well known that ROS and RNS also play an important role as secondary messengers in the orchestration of wound healing processes (130, 131). This idea of redox-based repair of destroyed tissue becomes important in connection with acute and chronic wound healing supported by CAP. There is some evidence that the Nrf2 pathway does not only function in cellular defense against increased ROS levels but it also has central regulatory effects in wound healing (Figure 4) (117, 132). The schematic overview in Figure 4 summarizes the state of knowledge on molecular patterns in wound healing in response to CAP treatment and aligns these results with insights from redox biology and research on molecular biology of healing processes in acute wounds (90, 117, 124, 132). Briefly, it is assumed that CAP treatment leads to a transient and reversible modification of proteins and the lipid bilayer, which contribute to normal or pathologic stages of wound healing (117, 140, 141). This is crucially mediated by the Nrf2 pathway (90, 116, 117). Its key role in up-regulation of detoxifying and antioxidant genes is mentioned above (113, 115). Moreover, via activation of Keap1, which does not only act as sensing element in the redox stress reaction of the Nrf2 pathway, CAP stabilizes the architecture of F-actin cytoskeleton and focal adhesions, and increases granulation tissue formation and matrix deposition (117, 132). As a key regulator in macrophages, Nrf2 mediates the infiltration of macrophages and neutrophils and the upregulation and secretion of pro- and anti-inflammatory ligands (e.g. TNFα, TGFβ, IL-1β etc.), which activate signaling and intracellular generation of reactive oxygen and nitrogen species (117).

Furthermore, CAP supports angiogenesis by recruiting endothelial cells, stimulates growth factor expression like keratinocyte growth factor (KGF), epidermal growth factor (EGF), or vascular epidermal growth factor (VEGF), and activates protein kinase B (Akt), which induces Nrf2 expression (70, 71, 138, 139). Nrf2-regulated inflammation and angiogenesis is also shown in numerous studies (133-137). Appropriate effects of CAP are also attributed to the regulation of Nrf2 (90, 116, 117).

Moreover, the activity of the transcription factor p53 depends on the stage of wound healing and reactive species concentration (90, 117). The tumor suppressor protein p53 influences cell proliferation and apoptosis and has a central role in angiogenesis and cell cycle regulation and DNA repair. When the expression of p53 is relatively low, p53 enhances the protein level of Nrf2 and its target genes promote cell survival depending on the cyclin-dependent kinase inhibitor 1 (p21). When p53 expression is high, the Nrf2-mediated survival response is inhibited by p53 (142, 143).

Taken together, CAP treatment leads to an accelerated repair in acute wounds. All these findings are mainly based on numerous in vitro and in vivo studies using the argon-driven cold atmospheric plasma jet kINPen (32, 34).

The long-term and systematic investigation of molecular biological processes of plasma-supplemented wound healing processes has opened several interconnections of plasma
medicine and redox biology. In wound healing, insights from redox biology, indicating that redox-sensitive processes are driving factors in tissue repair (130, 131), can serve as a sound scientific basis to confirm CAP applications in this field. There is no doubt that this may be true also for other fields of biomedical application of cold atmospheric plasma.

Medical Application of Physical Plasma – Present and Future

Besides wound healing, several other indications for plasma application in dermatology are being taken into consideration, mainly in the treatment of pathogen-based and/or inflammatory skin irritations and diseases (128, 144-146). Also, anti-infective plasma applications have been tested in ophthalmology (147-149), while plasma in dentistry is under research for several years, too. Possible dental applications include antimicrobial plasma activity, inactivation and removal of biofilm on teeth and on dental implants, disinfection of tooth root canal, plasma-assisted cleaning and optimization of tooth and implant surfaces to improve bone integration. Additionally, in-growth or bonding of dental fillings and prostheses, decontamination and coating of dental prosthesis, antimicrobial treatment of the oral mucosa, oral wound healing and tooth whitening are under investigation (150). For more details on promising clinical applications of CAP, see a recent review by Metelmann et al. (151).

As it was mentioned above, depending on plasma treatment intensity and time, it is possible to inactivate mammalian cells by initializing programmed cell death in them. This is true particularly for cancer cells. After several reports on apoptosis induction in cancer cells \textit{in vitro} (152-155), animal studies on transcutaneous plasma treatment of subcutaneously induced solid tumors could prove the general concept of plasma-supported tumor treatment (156, 157). However, there are several open questions about the mechanisms of plasma attack on cancer cells, a possible selectivity with regard to healthy tissue or on possible secondary effects distant from the region of local plasma treatment. Most current hypotheses are based on a predominant role of plasma-generated redox active species (158). Briefly, it is assumed that CAP treatment causes apoptosis of cancer cells through a selective rise of intracellular ROS and corresponding ROS-based death pathways. In that regard, enhanced sensitivity of cancer cells may be caused by enhanced ROS levels in the cancer resulting from its unique metabolic activities (113, 159). Other hypotheses attribute differences in cell sensitivity to significant variations of aquaporins (AQPs) among different cell lines. Enhanced generation of long-lived species, such as $\text{H}_2\text{O}_2$ via extracellular superoxide dismutase (Ex-SOD, SOD3) on the cytoplasmatic membrane of cancer cells and a subsequent trigger of immune attack on tumoral tissues \textit{via} $\text{H}_2\text{O}_2$-mediated \textit{(second messenger)} lymphocyte activation is also discussed (160, 161). Another interesting hypothesis is based on the specific action of CAP \textit{via} singlet oxygen ($^1\text{O}_2$) generation and the subsequent
induction of intercellular ROS-RNS-dependent apoptosis-inducing signaling (162). Finally, a plasma-induced stimulation of immunogenic cell death via damage associated molecular patterns (DAMPs) is under discussion (163, 164).

There are several promising experimental results leading to the situation that plasma application in cancer therapy is now one of the most attractive research fields in plasma medicine (155). Based on the experimental proof of inactivation of single layers of cancer cells by local plasma treatment (165), first of all a supportive plasma application in combination with surgical tumor resections in cases where large-scale tumor removal is impossible, seems to be realistic (166, 167). Moreover, first CAP applications in palliative care in patients with advanced squamous cell carcinoma of head and neck have not only resulted in the intended reduction of microbial load and resulting reduction of typical fetid odor, but in some particular cases also in transient tumor remission (168-170). Further research will tell us if any direct plasma application is useful for the reduction or complete removal of solid tumors and will lead to a “paradigm shift in cancer therapy” as it was predicted some years ago (156).

**Conclusion and Outlook**

It is a very interesting perspective to attribute vital processes to electron flow, *i.e.* energetic electrons are processed by biochemical and molecular biological pathways to transfer their energy into chemical energy to realize metabolic and signaling processes. From this point of view, redox gradients are eventually the driving forces of life (171). Because the primary process of generation of cold atmospheric plasma is the acceleration of electrons by electrical fields, plasma application may be considered as an initial part of a complex electron-transfer process transferring electrical energy via complex chemical reaction cascades into biological effects.

One of the main advantages of biomedical application of CAP is that the active components, such as ROS and RNS, are generated locally and only for the required duration of the application primarily by a physical process. By means of variations of several plasma parameters, the essential ROS and RNS-based energy transfer from plasma to cells and tissue can be easily controlled. This is the main reason why one can describe the biomedical plasma application as a field of applied redox biology.

The insight that CAP impact may result either in cell and tissue stimulation or in cell death, depending on exposure conditions (*e.g.* treatment time), fits very well with the theory of oxidative stress mainly introduced and developed by Sies (172-176). According to that, oxidative stress can be differentiated between oxidative eustress and oxidative distress depending on low or high oxidant exposure. These processes are strongly controlled by adaptive cellular...
responses, including the Nrf2 pathway that plays a central role above all in cell defence (115, 176, 177).

While CAP serves as a controllable source of redox-active species, the cellular environment and its antioxidative capacity may act as a “ROS-RNS sink”. The interaction of both components will define the degree of exposure of the living system to redox active species. Depending on the cellular ability of adaptive response as a third component in this process, either oxidative eustress or distress is resulting. In the case of CAP treatment this may result in stimulation of tissue regeneration or cell death (Figure 5).

Based on these insights, redox biology will not only serve as a scientific basis to further explain biological plasma effects. Conversely, CAP may become a useful tool for specific research in redox biology. It is obvious that both plasma medicine and redox biology are interested in similar questions:

i) Are there single and specific ROS and RNS responsible for distinct biological effects or is it only a matter of redox potential at the cellular target sites?

ii) How to identify and analyze specific ROS and RNS at their site of action?

iii) Which cell biological mechanisms are responsible for different sensitivity of several cell types to the impact of CAP as well as redox-active species?

iv) Is it possible to find a measure for biological plasma effects that can serve as a kind of “treatment dose”?

This preliminary small catalogue of questions can be easily extended considering the findings and future prospects of redox biology, both in view of basic research and with respect to specific pathologies (178). Finally, yet importantly, the concept of oxidative eustress and distress and its possible controllability by CAP treatment can also serve for further basic research on the “hormesis” phenomenon, which has received increased attention in recent years (176, 179-182).

Conflicts of Interest

The majority of research work that served as a scientific basis for further development and CE certification of the atmospheric pressure plasma jet kINPen MED as a medical device by neoplas tools GmbH Greifswald, Germany has been realized by INP Greifswald. INP Greifswald is a minority shareholder of neoplas tools GmbH Greifswald, Germany.

Authors’ Contributions

ThvW was responsible for the concept of the manuscript, review of literature and its text in general. AS, SB and KW contributed detailed content on mechanisms on CAP-supported wound healing, cellular redox mechanisms, and plasma chemistry, respectively. AS compiled and designed Figure 4. All authors reviewed the manuscript.

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