SYNTHESIS AND CHARACTERIZATION OF NANO BIOTRICALCIUM SILICATE, AS A COMPONENT OF AN ENDODONTIC SEALER

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ABSTRACT. Endodontic sealers are designed to be used in conjunction with semi-rigid materials during endodontic treatment, in order to obtain a three dimensional obturation of the root canal. During the last years, tricalcium silicate (C₃S), due to its increased biocompatibility, and superior physicochemical properties, has been investigated as an important component of endodontic filling materials. For most materials available on the market the source of C₃S alongside C₂S is MTA (mineral trioxide aggregate), but obtaining C₃S through synthesis is considered to be a much better alternative due to its superior purity and controlled size of the particles. In this study C₃S was synthetized in nanosized particles, by sol-gel method, from TEOS and calcium nitrate tetrahydrate without or with mineralizer NaF. A study was conducted in order to analyze the obtained powder and the hydrated samples which were prepared by mixing the powder with water in a ratio of 0.4, and cured for 28 days. The dried gels were thermally treated at 1450 ºC respectively at 1350 ºC. XRPD and TEM revealed the main presence of nanosized tricalcium silicate besides dicalcium silicate and small quantities of calcium hydroxides at both of synthesis temperatures. The hydration compounds evidenced by XRPD were calcium silicate hydrate alongside calcium hydroxide and calcium carbonate. FTIR analysis evidenced the specific vibration bands for O-H and Si-O bounds in hydrated calcium silicates.

Keywords: endodontic sealer, calcium silicate

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INTRODUCTION

Root canal obturation is the last phase of the endodontic treatment that will, if performed correctly, ensure the long-term success of the endodontic treatment [1]. The requirements for the ideal root canal filling material are multiple, and currently there is no such a material to fulfil all of them, even though there is a wide variety available on the market [2, 3].

In the last decades, as a progress in the field of nanotechnology new materials have been introduced in endodontics: bioceramic materials. Bioceramics are materials with increased biocompatibility such as alumina and zirconia, bioactive glass, glass ceramics, calcium silicates, calcium phosphates which can be biodegradable, bioinert or bioactive [4-6].

Tricalcium silicate (C₃S) is the main component of MTA (mineral trioxide aggregate), a cement with a similar composition with Portland cement, which has been successfully used in endodontic surgery and vital pulp therapy [7]. Lately C₃S was introduced as a main component of endodontic sealers, because of its outstanding biological and physicochemical properties.

Because endodontic obturation, will be in contact for a long period of time, with the periapical tissues, endodontic sealers which are genotoxic, mutagenic, carcinogenic will interfere with the periapical healing process. [8]. Compared to other materials, calcium silicate-based materials, due to their increased biocompatibility, do not induce an inflammatory response into periradicular tissues [9, 10].

Calcium silicate sealers exhibit excellent antibacterial properties better or at least similar to conventional sealers [2, 11, 12]. The lack of volumetric shrinkage upon setting, good adhesion to dentin, and lack of solubility makes them suitable for being placed in a moist environment [13]. Because of their hydrophilic properties, a certain amount of moisture is required to initiate the setting reaction, moisture that is provided by the dentine [14]. After the hydration process, a rigid matrix consisting of calcium silicate hydrates and calcium hydroxide is formed [15]. The calcium hydroxide released will exhibit antibacterial and anti-inflammatory properties and will induce bone mineralization [16, 17].

The bioactivity of calcium silicates was demonstrated in in vitro studies by the presence of a layer of calcium phosphates or even hydroxyapatite after soaking the samples in simulated body fluid (SBF) [18-20]. A large number of studies have been conducted in order to evaluate the properties of (tri)calcium silicates and the best method of their synthesis [21-25].
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Most calcium silicate-based materials for endodontic use, which are available on the market, consist of MTA. In order to obtain a new material, more biocompatible, with better physicochemical properties, a lower setting time, and a controlled size of the particles, the synthesis of calcium silicates as a main component of endodontic sealers became a necessity.

The main purpose of this study was to synthetize bio nano tricalcium silicates (C₃S) from TEOS, Si(OC₂H₅)₄, (tetraethyl orthosilicate) and Ca(NO₃)₂x4H₂O (calcium nitrate tetrahydrate) without or with mineralizer NaF by a sol-gel method, and characterize them for obtaining the endodontic sealer.

RESULTS AND DISCUSSIONS

Thermal analysis

Main thermal effects

The thermal analysis curves (TG/DSC) for the gel without additive, dried at 250 ºC, are displayed in Figure 1, and those for the mixture with NaF, dried at 120 ºC, are shown in Figure 2. In both cases, a 10 ºC /min heating rate up to 1400 ºC was performed.

Figure 1. Thermal behaviour of dried gel (250 ºC) without additive.
At lower temperatures (T < 200 °C) endothermic effects can be noticed, as a result of the removal of adsorbed water in the sample. In the 200-750 °C temperature range pronounced endothermic effects are visible, due to the elimination of hydrated water and decomposition of calcium nitrate tetrahydrate (Ca(NO₃)₂·4H₂O) and tetraethyl orthosilicate, Si(OC₂H₅)₄ (TEOS). The large exothermic peak that can be observed at about 1000 °C, corresponds to the crystallization of dicalcium silicates and the one at around the 1300 °C is attributed to the formation of tricalcium silicate.

The total weight loss for the sample without mineralizer, dried at 250 °C is 57.59 %, and for the sample with NaF dried at 120 °C is 72 %.

**X-ray powder diffraction (XRPD) of synthetized powders**

The XRPD patterns of synthesized calcium silicates at 1450 °C and 1350 °C are presented in Figure 3 a and b. The phase composition of the thermally treated powders, determined by XRPD, revealed the main presence of tricalcium silicate (C₃S), besides dicalcium silicate (C₂S) and calcium hydroxide Ca(OH)₂, as a result of hydration of calcium oxide, CaO. The presence of dicalcium silicate and calcium hydroxide indicates an incomplete reaction between reactants, but their presence in endodontic sealer would not be harmful to human cells.
SYNTHESIS AND CHARACTERIZATION OF NANO BIOTRICALCUM SILICATE, AS A COMPONENT OF AN ENDODONTIC SEALER

The crystallite sizes of tricalcium silicate were calculated from XRPD data using Scherrer formula. The average values for the C₃S obtained at 1450 ºC, was 41.51 nm and those for C₃S with mineralizer obtained at 1350 ºC was 54.78 nm.

Transmission electron microscopy (TEM)

TEM was used to illustrate the shape and morphology of mineral compounds. The presence of rhombohedral well-developed, nanometric-sized crystals of tricalcium silicate, besides of small quantities of hexagonal crystals of dicalcium silicate are illustrated in Figure 4.
Figure 4. TEM image of tricalcium silicate powder synthesized at 1450 °C (up) and 1350 °C (down).

Figure 4 (up) presents the shape and sizes of the powder synthesised at 1450 °C and figure 4 (down) for the powder obtained at 1350 °C. No differences can be observed in the characteristics of the calcium silicates minerals. Both syntheses led to rhombohedral shapes and nanometric sizes for tricalcium silicates.
Hydration mechanism of calcium silicates

In order to facilitate the use of calcium silicates as endodontic sealers, they have to be mixed with aqueous solutions. This ensures hardening which comes due to the crystallization of calcium silicate hydrates.

Calcium silicates hydration determines protons fixation, so O$^{2-}$ is changed into HO$^-$, SiO$_4^{4-}$ in H$_n$SiO$_4^{(n-4)}$, Ca$^{2+}$ ions in Ca$^{2+}$ Aq. HO$^-$ and Ca$^{2+}$ ions migrate in solution and a calcium silicate hydrate (CSH) layer is formed on the calcium silicate surface. This layer is preponderantly constituted from H$_3$SiO$_4$– and H$_4$Si$_2$O$_7^{2-}$ ions.

The schematic reactions of tri- and dicalcium silicates are illustrated in Eq. 1 and 2.

\[ 2(Ca_3Si_2O_7) + 6H_2O \rightarrow Ca_3Si_2O_7\cdot 3H_2O + 3Ca(OH)_2 \]  
C$_3$S \hspace{2cm} \text{CSH}  
\[ 2(Ca_2Si_2O_4) + 4H_2O \rightarrow Ca_3.3Si_2O_7\cdot 3H_2O + 0.7Ca(OH)_2 \]  
C$_2$S \hspace{2cm} \text{CSH}  

During the hydration, the thickness of the calcium silicate hydrate (CSH) layer and the index of crystallinity are increased. The hydration process is slow depending on the diffusion rate of the ions inside the new formed layer and the ion change from solid to solution.

XRDP of hydrated calcium silicates

The XRDP patterns of synthetized samples at 1450 °C, after the hydration process, cured for 28 days in 90 % relative humidity at 22 °C, and 37 °C, are shown in Figure 5 a and b.
The hydration compounds evidenced by XRPD are hydrated calcium silicate (CSH) alongside calcium hydroxide, calcium carbonate and dicalcium silicate (C_2S). The crystallinity index of CSH is low for both samples due to the short time of hydration, higher for the sample cured at 37 °C (Figure 4b). The calcium hydroxide is evidenced in the pattern as a hydration product of calcium silicates. The presence of CO_2 in the environment and its partial reaction with Ca(OH)_2 explains the presence of CaCO_3 crystals. As observed from Figure 5, C_2S is present in both samples. The presence of C_2S could be due to its long-time necessity for hydration or due to its high grain size.

The crystallite sizes of calcium silicates hydrates were calculated from XRPD data using Scherrer formula. The average values were 26.59 nm for samples cured at 22 °C and 22.39 nm for samples cured at 37 °C.
FTIR analysis for hydrated calcium silicates

The FTIR spectra for hydrated calcium silicates, after the hydration process, cured at 22 °C respectively at 37 °C for 28 days, are presented in Figure 6 a and b.

![Figure 6. FTIR spectra for C₃S cements cured for 28 days at (a) 22 °C and (b) 37 °C, respectively.](image)

Due to the hydration process two broad absorption bands around the 1400 -1600 cm⁻¹ and 3400 – 3600 cm⁻¹ are caused by the bending vibration of bound water incorporated in hydrated calcium silicates. The peak at 3630 cm⁻¹ corresponds to Ca(OH)₂, which is formed during the hydrolysis of silicate phases.
The specific vibration bands of Si-O bonds from SiO$_4$ groups for silicates can be evidenced. High spectral intensity bands are observed from $\sim$900 cm$^{-1}$ to $\sim$1000–1100 cm$^{-1}$, which suggests some rearrangements in the silica subsystem in the presence of water. These features reflect the dissolution of calcium silicates (C$_3$S, C$_2$S) and the polymerization of calcium silicate hydrate CSH. The small absorption band around 1081 cm$^{-1}$ could be attributed to both the vibration of the CO$_3^-$ group in the newly formed carbonates and the stretching vibration of Si-O bound in calcium silicate hydrates.

CONCLUSIONS

Tricalcium silicate (C$_3$S), was successfully synthesized at 1450 ºC respectively 1350 ºC from TEOS and calcium nitrate tetrahydrate without and with mineralizer by a sol-gel method. X-ray powder diffraction (XRPD) revealed the main presence of tricalcium silicates (C$_3$S), alongside dicalcium silicate (C$_2$S) and small quantities of calcium hydroxides Ca(OH)$_2$, at both synthesis temperatures. In samples cured for 28 days, the compounds evidenced by XRPD were calcium silicate hydrates (CSH), calcium hydroxide Ca(OH)$_2$ and calcium carbonate CaCO$_3$.

FTIR spectroscopy confirmed the presence of specific bands corresponding to the hydrated compounds in the solid. TEM images showed the well-developed nanocrystals of tri- and dicalcium silicates.

The data obtained revealed that the powder consists mainly of nanosized tricalcium silicates, with a good hydration rate, making it suitable for endodontic use.

EXPERIMENTAL PART

Synthesis of tricalcium silicate

In order to synthesize tricalcium silicate (Ca$_3$SiO$_5$)$_n$, calcium nitrate tetrahydrate (Ca(NO$_3$)$_2$ x4H$_2$O, 99.5 % purity, Merck) and tetraethyl orthosilicate, (TEOS - C$_8$H$_{20}$O$_4$Si, Merck), were used as main raw materials. Ethanol (C$_2$H$_5$OH) and nitric acid (HNO$_3$) were used as pH regulators. In order to reach calcium silicate stoichiometry the molar ratio of CaO/SiO$_2$ was established at 3/1.
The flowchart of steps involved in the tricalcium silicate synthesis is presented in Figure 7.

The homogenized mixture of TEOS, calcium nitrate, ethanol, and nitric acid, was dried at 60 °C for gelation. The resulted gel was further dried at 120 °C and, afterwards, thermally treated at 1450 °C for 4 hours.

In the other mixture, in order to facilitate the reaction between compounds and to reduce the temperature of thermal treatment, an additive of NaF (1 %) was added in the homogenization step. After drying the obtained gel was thermally treated in two steps: at 600 °C for 6 hours and at 1350 °C for 30 minutes.
Characterization of C₃S powder

X-ray powder diffraction (XRPD)

The phase composition of C₃S powder was determined using a Bruker D8 Advance diffractometer, with Co, Kα₁ = 1.79026 Å, operated at 35 kV and 40 mA. The pattern was collected for 2θ range from 5° to 65°, with a step size of 0.02 °/sec.

Transmission Electron Microscopy (TEM)

The size and shape of calcium silicate crystallites were investigated by TEM on HITHACHI H-7650 equipment.

Thermal analysis

The thermal behaviour of gels obtained by the sol-gel method, was studied by thermal analysis, conducted by the thermogravimetric (TG) and differential scanning calorimetry (DSC) using a TA Instruments DSC SDT Q600 thermogravimetric analyser.

Fourier transform infrared (FTIR) spectroscopy

The FTIR absorption spectra were recorded with a JASCO V-670 UV–Vis-NIR spectrophotometer.

REFERENCES

1. J. Branstetter; J.A. von Fraunhofer; J. Endod., 1982, 8(7), 312-316.
2. H.M. Zhou; Y. Shen; W. Zheng; L. Li, Y.F. Zheng, M. Haapasalo, J. Endod., 2013, 39(10), 1281-1286.
3. D. Orstavik, Endodontic Topics, 2005, 12(1), 25-38.
4. S. Utneja; R.R. Nawal; S. Talwar; M. Verma; Restor. Dent. Endod., 2015, 40(1), 1-13.
5. K. Koch; D. Brave, Dentaltown, 2009, 39-43.
6. L. Bizo; K. Sabo; R. Barabas; G. Katona; L. Barbu-Tudoran; A. Berar; Studia UBB Chemia, LXV, 1, 2020, 137-148.
7. N. Meschi, X. Li, G. Van Gorp, J. Camilleri, B. Van Meerbeek, P. Lambrechts, Dent Mater, 2019, 35(9), 1342-1350.
8. F.C. Martinho; S.E.A. Camargo; A.M.M. Fernandes; M.S. Campos; R.F. Prado; C.H.R. Camargo; M.C. Valera; International Endodontic Journal, 2018, 51, 41-57.
9. D. Brave; A.A. Nasseh; K. Koch; Roots, 2013, 4(4), 6-12.
10. E.J. Silva; P.M. Senna; G. De-Deus; A.A. Zaia; Int. Endod. J., 2016, 49(6), 574–580.
11. S. Jitaru; I. Hodisan; L. Timis; A. Lucian; M. Bud; Clujul Med., 2016, 89(4), 470-473.
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12. H. Zhang; Y. Shen; N.D. Ruse; M. Haapasalo; J. Endod., 2009, 35(7), 1051–1055.
13. A. Avram; M. Gorea; R. Balint; L. Timiș; S. Jitaru; A. Mocanu; M. Tomoaia-Coișel; Studia UBB Chemia, LXII, 4, Tom I, 2017, 81-92.
14. G.C. Gritti; S.I.A. Cavalcante; E.M. Maia-Filho; J. Bauer; M.C. Bandéca; G. Gavini; C.N. Carvalho; Braz. Oral Res., 2017, 31, e76.
15. B. Darvell; R.C.T. Wu; Dent. Mater., 2011, 27, 407-422.
16. H.K. El-Hamid; H.H. Abo-Almaged; M.M. Radwan; J. App. Pharm. Sci., 2017, 7(10), 001-008.
17. A. Koutroulis, S.A. Kuehne, P.R. Cooper, J. Camilleri, Sci. Rep., 2019; 9, 19019.
18. W. Zhao, J. Chang, Mater. Lett., 2004, 58, 2350-2353.
19. X. Liao, H. Zhu, G. Yin, Z. Huang, Y. Yao, X. Chen, Bull. Mater. Sci., 2011, 34, 1151–1155.
20. M.C. Jimenez-Sanchez; J.J. Segura Egea; A. Diaz-Cuenca; J. Clin. Exp. Dent. 2019, 11(4), e322-326.
21. M. Wu; T. Wang; Y. Wang; F. Li; M. Zhou; X. Wu; Mater. Lett., 2018, 227, 187-190.
22. P. Torkittikul, A. Chaipanich, Mater. Sci. Eng. C, 2012, 32, 282-289.
23. K.B. Willbank, S.A. Schwartz, W.G. Schindler, J. Endod., 2007, 33(10), 1235-1238.
24. L. Wang, X. Xie, C. Li, H. Liu, K. Zhang, Y. Zhou, X. Chang, H.H. K. Xu., J. Dent., 60, 2017, 25-35.
25. L. Grech, B. Mallia, J. Camilleri, Dent. Mater., 29, 2013, 20-28.