Assessment of the Tumor Redox Status in Head and Neck Cancer by $^{62}$Cu-ATSM PET

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Abstract

Purpose
Tumor redox is an important factor for cancer progression, resistance to treatments, and a poor prognosis. The aim of the present study was to define tumor redox (over-reduction) using $^{62}$Cu-diacetyl-bis(N4-methylthiosemicarbazone) ($^{62}$Cu-ATSM) PET and compare its prognostic potential in head and neck cancer (HNC) with that of 2-deoxy-2-[18F]fluoro-D-glucose ($^{18}$F-FDG).

Methods
Thirty HNC patients (stage II–IV) underwent pretreatment $^{62}$Cu-ATSM and $^{18}$F-FDG PET scans. Maximum standardized uptake values (SUV$^{\text{ATSM}}$ and SUV$^{\text{FDG}}$) and tumor-to-muscle activity concentration ratios (TMR$^{\text{ATSM}}$ and TMR$^{\text{FDG}}$) were measured. Reductive-tumor-volume (RTV) was then determined at four thresholds (40%, 50%, 60%, and 70% SUV$^{\text{ATSM}}$), and total-lesion-reduction (TLR) was calculated as the product of the mean SUV and RTV for $^{62}$Cu-ATSM. In $^{18}$F-FDG, metabolic-tumor-volume (MTV) and total-lesion-glycolysis (TLG) were obtained at a threshold of 40%. A ROC analysis was performed to determine % thresholds for RTV and TLR showing the best predictive performance, and these were then used to determine the optimal cut-off values to stratify patients for each parameter. Progression-free-survival (PFS) and cause-specific-survival (CSS) were evaluated by the Kaplan-Meier method.

Results
The means ± standard deviations of PFS and CSS periods were 16.4±13.4 and 19.2±12.4 months, respectively. A ROC analysis determined that the 70% SUV$^{\text{ATSM}}$ threshold for RTV and TLR was the best for predicting disease progression and cancer death. Optimal cut-offs for each index were SUV$^{\text{ATSM}} = 3.6$, SUV$^{\text{FDG}} = 7.9$, TMR$^{\text{ATSM}} = 3.2$, TMR$^{\text{FDG}} = 5.6$, RTV = 2.9, MTV = 8.1, TLR = 14.0, and TLG = 36.5. When the cut-offs for TMR$^{\text{ATSM}}$ and TLR were set as described above in $^{62}$Cu-ATSM PET, patients with higher TMR$^{\text{ATSM}}$ (p = 0.03) and...
greater TLR (p = 0.02) showed significantly worse PFS, while patients with greater TLR had significantly worse CSS (p = 0.02). Only MTV in $^{18}$F-FDG PET predicted differences in PSF and CSS (p = 0.03 and p = 0.03, respectively).

**Conclusion**

Tumor redox parameters measured by $^{62}$Cu-ATSM PET may be determinants of HNC patient outcomes and help define optimal patient-specific treatments.

**Introduction**

The tumor microenvironment is characterized by hypoxia (a low partial pressure of oxygen: a low pO$_2$) and a highly reducing redox status [1–3]. Cancer cells are capable of surviving under hypoxic conditions by inducing the expression of metabolic enzymes required for anaerobic metabolism such as glycolysis. They may also induce the formation of blood vessels by a process called angiogenesis in order to fulfill their oxygen and nutritional requirements. However, new blood vessels are often poorly formed, thereby leading to an unstable cancer environment that oscillates between low and moderate to high oxygen conditions. This cycling phenomenon is termed cycling hypoxia. An over-reductive state is the state in which cancer cells and tissues contain excessive levels of electrons relative to O$_2$, which is caused by impaired respiratory chains or hypoxia, and oxidative stress is induced by excess reactive oxygen species (ROS) produced from O$_2$ and redundant electrons due to mitochondrial dysfunction. Evidence to suggest the importance of the redox status for cancer progression, resistance to treatments, and a poor prognosis is mounting [4–10] (Fig 1).

In order to measure the tumor redox status *in vivo*, magnetic resonance imaging (MRI) with redox-sensitive contrast agents has been performed on animal models [11, 12]. Copper (II) diacetyl-bis(N$^4$-methylthiosemicarbazone) (Cu-ATSM) is one of the two main hypoxia-seeking ligands for positron emission tomography (PET), with the other being fluorinated 2'-nitroimidazoles represented by $^{18}$F-fluoromisonidazole ($^{18}$F-FMISO) [13, 14]. Previous studies reported that a good correlation existed between low pO$_2$ directly measured by polarographic oxygen electrodes and high tracer accumulation *in vivo* [15, 16]. However, discrepancies have been identified between the distributions of Cu-ATSM and FMISO in different tumor tissue types [17, 18]. Although the Cu(II)-ATSM retention mechanism is not yet fully understood [19–22], Cu(II)-ATSM PET may be reassessed as tumor over-reduction imaging that is distinctive from PET with fluorinated nitroimidazoles (FR-NO$_2$) (Fig 2). Cu(II)-ATSM is a neutral lipophilic molecule that easily penetrates cell membranes. In cancer cells over-reduced due to mitochondrial dysfunction and hypoxia, Cu(II)-ATSM may be converted to [Cu(I)-ATSM]$^-$ with electrons (e$^-$) supplied from abnormally reduced mitochondria in a number of forms including NADH and NADPH, and retained in cells because of its negative charge. Cu(I) is subsequently dissociated by reactive chemical species (RS) generated in the reduced condition and is irreversibly trapped as Cu(I)-RS in cells. FR-NO$_2$ passes through cell membranes by slow diffusion and may be converted to a reduced form, FR-NO$_2^-$, by xanthine oxidoreductase [19]. Under hypoxic conditions (low pO$_2$), FR-NO$_2^-$ may be reduced further by intracellular reductases in a low oxygen concentration-dependent manner to R-NH$_2$, which binds covalently to macromolecules in cancer cells. The accumulation of FR-NO$_2$ is subject to a low oxygen concentration, while Cu-ATSM uptake is assumed to reflect the imbalanced redox (over-reductive) status in cancer cells. We herein defined a new concept of 'tumor redox imaging
with Cu-ATSM PET, which means Cu-ATSM may be used distinctively from FR-NO₂ in order to determine the imbalanced redox (over-reductive) status in cancer cells, which is important for appropriate treatment strategies and prognoses.

Glycolysis is generally accelerated in cancer cells even in the presence of oxygen (the Warburg effect), which enables 2-deoxy-2-[¹⁸F]fluoro-D-glucose (¹⁸F-FDG) PET to determine the cancer stage, monitor treatment responses, and predict long-term prognoses. The predictive value of ¹⁸F-FDG PET for the prognoses of patients with head and neck cancer (HNC) has recently been reported, particularly using volume-based metabolic parameters such as metabolic-tumor-volume (MTV) and total-lesion-glycolysis (TLG) [23–25]. We recently reported that the intensity-based parameters of ⁶²Cu-ATSM PET (standardized uptake value: SUV and tumor-to-muscle activity ratio: TMR) may be better prognostic markers than those of ¹⁸F-FDG PET in HNC [26]. On a ⁶²Cu-ATSM PET intensity basis, HNC patients with the higher tumor accumulation of ⁶²Cu-ATSM had significantly worse prognoses than those with low-uptake tumors. In contrast, no significant difference was observed in prognoses between HNC patient groups showing higher and lower ¹⁸F-FDG uptakes.
The aim of the present study was to investigate the predictive performance of $^{62}$Cu-ATSM and $^{18}$F-FDG PET-derived parameters of lesion image intensity and volume in HNC. To the best of our knowledge, no study has yet defined $^{62}$Cu-ATSM PET as over-reduction imaging in tumors or evaluated the value of volumetric PET parameters with $^{62}$Cu-ATSM reflecting a reductive tumor burden for prognostic predictions.

Materials and Methods

Patients

Thirty untreated patients (24 males, 6 females; 68.3 ± 12.4 years of age) with biopsy-proven stage II to IV HNC at the University of Fukui Hospital between April 2007 and October 2012
were enrolled in this prospective study (Table 1). The primary tumor sites were the oral cavity ($n = 9$), paranasal sinus ($n = 5$), oropharynx ($n = 5$), hypopharynx ($n = 2$), larynx ($n = 3$), salivary gland ($n = 5$), and other ($n = 1$). Histologies were 24 squamous cell carcinomas and 6 adenocarcinomas. All patients underwent CT and magnetic resonance imaging scans in order to obtain local information as well as whole-body $^{18}$F-FDG PET/CT scans for staging. Each patient underwent $^{62}$Cu-ATSM PET within a week of the $^{18}$F-FDG PET/CT scan. This study was approved by the Ethics Committee of the University of Fukui, Faculty of Medical Sciences. Written informed consent was obtained from all individual participants included in the study. In this prospective study, we increased the number of patients from that in our previous study with HNC and also extended follow-up periods [26].

### Preparation of $^{62}$Cu-ATSM

$^{62}$Cu glycine (non-carrier added $^{62}$Cu) solution was obtained from a $^{62}$Zn/$^{62}$Cu generator system every hour [27, 28]. $^{62}$Cu-ATSM was prepared with a simple mixture of $^{62}$Cu solution (5 mL) and 0.2 mL of ATSM solution (0.5 mM in dimethyl sulfoxide) in a sterilized vial [15]. The radiochemical purity of $^{62}$Cu-ATSM was confirmed with high-performance liquid chromatography (HPLC) using authentic unlabeled Cu-ATSM prior to the first injection administered to patients.

### PET Procedure

PET procedures were described in detail in our previous study [26]. Briefly, a whole-body PET scanner (Advance, General Electric Medical Systems, Milwaukee, WI) was used for $^{62}$Cu-ATSM PET studies and a 20-minute dynamic PET image acquisition, including known primary tumor sites, was performed after an intravenous injection of 600 to 800 MBq (approximately 16–22 mCi) of $^{62}$Cu-ATSM over 30 seconds. The dynamic frames were 10 seconds $\times$ 12 frames, 60 seconds $\times$ 8 frames, and then 5 minutes $\times$ 2 frames. $^{18}$F-FDG PET images were acquired in the static mode with a whole-body PET/CT scanner (Discovery LS, General Electric Medical Systems, Milwaukee, WI) approximately 50 minutes after the administration of 185 MBq (5 mCi) of $^{18}$F-FDG. All patients fasted for at least 4 hours before the $^{18}$F-FDG PET study.

PET images of $^{62}$Cu-ATSM and $^{18}$F-FDG were reconstructed using the iterative reconstruction method with 14 subsets and 2 iterations with a spatial resolution of 6-mm full width at half maximum.
half maximum. The reconstructed images were converted to semiquantitative images parameterized in units of SUV.

Image Analysis
The time-activity curves of $^{62}$Cu-ATSM PET obtained from dynamic data showed that all tumors had stable radiotracer retention by 8–10 minutes post-injection and in the later phase after the tracer injection [26–28]. Thus, an average image of the last 10-minute frame, which was considered appropriate scan timing for the tracer retention phase from time-activity curves (TACs), was used to evaluate the tumor redox status.

$^{62}$Cu-ATSM and $^{18}$F-FDG PET images were co-registered based on their respective CT images from PET/CT using automatic registration software (AW VS4, GE Medical Systems, Milwaukee, WI). Volumes of interest (VOIs) were drawn on the primary tumor and bilateral sternocleidomastoid muscles. Regarding intensity-based parameters, the overall tumor uptake of $^{62}$Cu-ATSM was assessed semiquantitatively on late-phase images by determining the maximum SUV ($SUV_{ATSM}$) and tumor-to-muscle activity concentration ratio ($TMR_{ATSM}$) using tumor SUV$_{ATSM}$ and muscle SUVs. The maximum SUV ($SUV_{FDG}$) and tumor-to-muscle activity concentration ratio ($TMR_{FDG}$) were determined in the same manner for $^{18}$F-FDG PET. Tumor contours were delineated to include voxels presenting SUV values greater than 40%, 50%, 60%, and 70% SUV$_{ATSM}$ for $^{62}$Cu-ATSM PET in order to determine optimal % thresholds for further analyses and 40% SUV$_{FDG}$ for $^{18}$F-FDG PET. The threshold of 40% SUV$_{FDG}$ for $^{18}$F-FDG PET was based on a previous study [29]. Tumor volumes were defined as reductive-tumor-volume (RTV) for $^{62}$Cu-ATSM and MTV for $^{18}$F-FDG. Total-lesion-reduction (TLR) was calculated as the product of average SUV and RTV for $^{62}$Cu-ATSM, and TLG was calculated as the product of the mean SUV and MTV for $^{18}$F-FDG.

Statistical Analysis
In an attempt to determine whether the tumor uptake and volume of $^{62}$Cu-ATSM or $^{18}$F-FDG were predictive of treatment outcomes, a correlation analysis was performed between the results of PET and those of clinical follow-ups. The physician who assessed patients for disease progression and survival was blinded to the results of the $^{62}$Cu-ATSM and $^{18}$F-FDG PET studies.

A receiver-operating-characteristic (ROC) analysis was performed in order to determine the % thresholds for volume-based redox parameters (RTV and TLR) showing the best predictive performance based on the area under the curves (AUCs) and optimum cut-off values for each PET index in order to identify patients with or without events (disease progression and overall death) at the time of the last follow-up after the treatment. The significance of differences between the AUCs was tested using the pairwise comparison of DeLong et al. [30]. A ROC analysis and comparison of AUCs were performed using MedCalc® (version 13.3.0.0; MedCalc Software bvba). The Kaplan-Meier method was used to assess the relationships between each PET parameter and progression-free survival (PFS) and cause-specific survival (CSS) rates. The equivalence of survival curves was tested with Log-rank (Mantel-Cox) statistics using GraphPad Prism® (version 6.01; GraphPad Software, Inc.). A probability of less than 0.05 was considered significant.

Results
Patient Characteristics
The characteristics of all 30 patients are summarized in Table 1. Fourteen patients received chemoradiation therapy (CRT) and underwent surgical operations (SOs), twelve received CRT,
one received radiation and underwent SO, and three underwent SO. Patients were clinically followed for periods ranging between 4 and 36 months (mean ± SD = 19.2 ± 12.4 months). At the last follow-up, 16 patients were alive for periods ranging between 7 and 36 months (mean ± SD = 27.6 ± 10.3 months): 13 with good control (complete response) and 3 with recurrence. Twelve patients died from local recurrence or metastasis of the primary cancer and 2 died from other diseases. The mean periods of PFS and CSS were 16.4 ± 13.4 months and 19.2 ± 12.4 months, respectively.

Survival Prediction

Among the thresholds of 40%, 50%, 60%, and 70% SUV_{ATSM} for volume-based redox indices (RTV and TLR), ROC analyses showed that the AUCs of RTV_{40%}, RTV_{50%}, RTV_{60%}, and RTV_{70%} were 0.56, 0.55, 0.56, and 0.64 for predicting disease progression and 0.58, 0.57, 0.58, and 0.68 for cancer death, respectively. Similarly, the AUCs of TLR_{40%}, TLR_{50%}, TLR_{60%}, and TLR_{70%} were 0.61, 0.62, 0.60, and 0.65 for predicting disease progression and 0.55, 0.56, 0.57, and 0.64 for cancer death, respectively. Although no significant difference was observed among AUCs, we selected a threshold of 70% SUV_{ATSM} as the optimum threshold value parameter for predicting disease progression and cancer death because it yielded the largest AUCs.

In all 30 patients, SUV_{ATSM} (mean ± SD) was 4.1 ± 1.9 (g/ml), SUV_{FDG} was 10.8 ± 5.2 (g/ml), TMR_{ATSM} was 4.0 ± 1.8, TMR_{FDG} was 9.2 ± 4.7, RTV was 4.1 ± 3.8 (ml), MTV was 16.8 ± 15.7 (ml), TLR was 13.2 ± 11.8 (g), and TLG was 130.5 ± 181.5 (g).

Optimum cut-off values determined by the ROC analysis for each PET index to divide patients with or without events were as follows: SUV_{ATSM} = 3.6, SUV_{FDG} = 7.9, TMR_{ATSM} = 3.2, TMR_{FDG} = 5.6, RTV = 2.9, MTV = 8.1, TLR = 14.0, and TLG = 36.5. When the cut-off values for TMR_{ATSM} and TLR were set as described above for 62Cu-ATSM PET, patients with higher TMR_{ATSM} had significantly worse PFS (p = 0.03), while those with greater TLR had significantly worse PFS and CSS (p = 0.02 and p = 0.02, respectively) (Figs 3A, 4A and 4B). Only MTV in 18F-FDG PET predicted differences in PFS and CSS (p = 0.03 and p = 0.03, respectively) (Fig 5A and 5B). SUV_{ATSM}, SUV_{FDG}, TMR_{FDG} (Fig 3B), RTV, and TLG did not show significant differences in PFS or CSS between the two groups.

Representative Cases

Fig 6 shows a 62-year-old man with tongue cancer (SUV_{ATSM} = 4.6, SUV_{FDG} = 10.1). Using thresholds of 70% SUV_{ATSM} and 40% SUV_{FDG} to delineate tumor contours, volume-based redox and metabolic parameters were calculated as follows: RTV = 3.6, MTV = 19.3, TLR = 12.8, and TLG = 115.9. He is still alive without any recurrence or metastasis after being treated (CRT + SO). The volume-based redox parameter, TLR, which was smaller than the cut-off value, correctly predicted his outcome. On the other hand, volume-based metabolic indices were greater than each cut-off value.

Fig 7 shows a 64-year-old man with right parotid cancer (SUV_{ATSM} = 6.9, SUV_{FDG} = 8.8). Using thresholds of 70% SUV_{ATSM} and 40% SUV_{FDG} to delineate tumor contours, volume-based redox and metabolic parameters were calculated as follows: RTV = 5.9, MTV = 6.3, TLR = 32.0, and TLG = 30.0. He developed iliac bone metastasis 15 months after being treated (CRT + SO). The volume-based redox parameters, RTV and TLR, which were greater than each cut-off value, correctly predicted his outcome. On the other hand, volume-based metabolic indices were smaller than each cut-off value.
Fig 3. Kaplan-Meier curves of progression-free survival (PFS) for $^{62}$Cu-ATSM PET (a) and $^{18}$F-FDG PET (b) in patients with HNC. Two groups of high (dotted lines) and low (solid lines) tracer accumulation were determined by each cut-off value of the tumor-to-muscle ratios (TMR$_{ATSM}$ and TMR$_{FDG}$). TMR$_{ATSM}$, one of the intensity-based redox parameters, showed a significant difference in PFS between two groups ($p = 0.03$), whereas TMR$_{FDG}$, one of the intensity-based metabolic parameters, did not ($p = 0.15$). The three-year PFS rate
Discussion

High tumor uptakes of $^{62}\text{Cu-ATSM}$ (TLR) as well as a high intensity ($\text{TMR}_{\text{ATSM}}$) predicted poor prognoses in HNC patients, as determined by PFS and CSS. These results indicate the importance of detecting tumor over-reductive states, namely, a reductive intensity and reductive tumor burden for the biological characterization of tumors and survival prediction. $^{62}\text{Cu-ATSM}$ PET imaging of an over-reductive state has potential as a marker for oxidative stress induced by the excessive production of ROS in cancer cells; it may provide information on the degree and amount of ROS in tumors, which drive cancer cell motility, invasion, tumor progression, and treatment resistance. We previously demonstrated that Cu-ATSM accumulated in regions rich in cancer cells expressing CD133, which is a frequently used marker for cancer stem cells or cancer stem cell-like cells [31], and a relationship has since been suggested to exist between these cells and poorer patient outcomes. Regarding metabolic PET parameters with $^{18}\text{F-FDG}$ in the present study, the predictive performance of MTV for HNC patient outcomes was good, whereas intensity-based metabolic parameters ($\text{SUV}_{\text{FDG}}$ and $\text{TMR}_{\text{FDG}}$) had a poor predictive value. Information obtained on oxidative stress in tumors by $^{62}\text{Cu-ATSM}$ PET may provide more accurate predictions of patient outcomes than glucose metabolism by $^{18}\text{F-FDG}$ PET. In any case, since cycling hypoxia, redox, and glycolytic activity in tumors may interact in diverse ways [1–3], the dynamics of the tumor microenvironment need to be revealed by future molecular imaging researches.

The over-reductive status is not the only determinant of Cu-ATSM retention in cancer cells because intracellular pH and copper metabolism may also affect the retention of the tracer [32, 33]. However, previous studies, including ours, demonstrated that the uptake of Cu-ATSM correlated with poor patient prognoses in some cancer types, such as HNC, cervical cancer, and rectal cancer [26, 34–36]. Tateishi et al. recently reported that the uptake of $^{62}\text{Cu-ATSM}$ was significantly higher in glioblastoma (WHO grade IV) than in lower-grade gliomas [37, 38]. The higher accumulation of $^{62}\text{Cu-ATSM}$ may reflect more ROS being produced in tumors as well as a more aggressive tumor phenotype [4–10]. Cu-ATSM PET delineates aggressive or treatment-resistant regions in tumors and this information may potentially be used for intensity-modulated radiation therapy (IMRT) planning and prognostic predictions for patients with these cancer types [39, 40].

Furthermore, the tumor redox status imaged by Cu-ATSM PET may provide criteria for redox-modulating strategies in cancer patients [41–48]. In non-cancerous cells, ROS play an essential role as second messengers in the normal regulation of various physiological processes. In cancer cells under mitochondrial dysfunction or hypoxia, they also act as signaling molecules to increase aggressiveness/motility/invasion and resistance to treatments, thereby leading to a worse prognosis with an increase in ROS production. On the other hand, lethal concentrations of ROS may trigger cell death pathways against the antioxidant capacity of cancer cells. Redox-modulating strategies to target these biochemical properties of cancer cells will represent a feasible therapeutic approach that may enable therapeutic selectivity and overcome resistance to treatments. Fig 8 shows a hypothetical relationship between excess ROS production levels, cancer cell states, and treatment options. Since the excessive production of ROS induces apoptosis in cancer cells or the progression of cancer growth, these strategies have been divided into two categories: to increase or reduce cellular ROS levels. Increases in intracellular oxidative stress have long been recognized as one of the mechanisms of action of cancer chemotherapy.
Two groups with the accumulation of large (> 14.0, dotted lines) and small (≤ 14.0, solid lines) amounts of $^{62}$Cu-ATSM were determined by total-lesion-reduction (TLR), one of the volume-based redox parameters. The two groups showed significant differences in PFS ($p = 0.02$) and CSS ($p = 0.02$). Three-year PFS and CSS rates were 61% and 67% for patients with a smaller reductive tumor burden (TLR ≤ 14.0), and 14% and 20% for those with a greater reductive tumor burden (TLR > 14.0), respectively.
Fig 5. Kaplan-Meier curves of progression-free survival (PFS) (a) and cause-specific survival (CSS) (b) in patients with HNC. Two groups with the accumulation of large (> 8.1, dotted lines) and small (≤ 8.1, solid lines) volumes of 18F-FDG were determined by metabolic-tumor-volume (MTV), one of the volume-based metabolic parameters. The two groups showed significant differences in PFS (p = 0.03) and CSS (p = 0.03). Three-year PFS and CSS rates were 70% and 73% for patients with a smaller metabolic volume (MTV ≤ 8.1), and 30% and 37% for those with a larger metabolic volume (MTV > 8.1), respectively.

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Multidisciplinary therapy (the combination of SO, RT, and CT) may effectively induce lethal injuries in cancer cells when combined with drugs that increase the production of ROS \[41, 42\]. In contrast, antioxidants may effectively prevent tumor progression, particularly in some kinds of cancer patients showing low levels of excess ROS \[43–46\]. They may also be used prophylactically for patients in remission in order to prevent recurrence or secondary cancer \[47, 48\].

Since no previous Cu-ATSM PET studies evaluated optimal segmentation methods for delineating over-reductive areas in tumors, four thresholds (40%, 50%, 60%, and 70% SUV\textsubscript{ATSM}) were examined by the ROC analysis in the present study. The threshold of 70% SUV\textsubscript{ATSM} was selected because it yielded the largest AUCs for predicting disease progression and cancer death. However, no significant difference was observed among the AUCs of the four thresholds. Thresholds of 80% or higher % SUV\textsubscript{ATSM}, which may more accurately predict
patient outcomes, need to be examined in future studies. It is important to note that optimal thresholds need to be obtained separately in each site because the volume definition using % thresholds varies with maximum SUV itself, which may differ among institutes using different PET scanners with different crystals, imaging, and reconstruction protocols. Other thresholding techniques using absolute values such as SUVs also need to be evaluated in the future. Furthermore, it is important to note that Cu-ATSM PET detects surplus electrons in some forms of reductants and does not directly reflect the degree and distribution of ROS in cancer tissues. Further fundamental and clinical validation studies are warranted.

In vivo mapping of the tumor redox status has been intensively examined in recent years. MRI with redox-sensitive T1 shortening or paramagnetic chemical exchange saturation transfer (CEST) contrast agents are used to evaluate the tumor redox state and its heterogeneity [11, 12]. Although this MR technique enables non-invasive observations of deep tissues, it is still being developed using animal models and requires a high-magnetic field MRI apparatus such
as 7 tesla. In contrast, $^{62}$Cu-ATSM is produced by a $^{62}$Zn/$^{62}$Cu generator with synthesis kits, which allows tumor redox PET imaging in humans to be performed conveniently on site. Integrated PET/MR scanners will enable the accurate registration and superimposed display of over-reductive areas in tumors detected by Cu-ATSM PET and MR signals from hydrogen protons ($^1$H) including information on metabolites by MR spectroscopy. Keshari et al. recently developed hyperpolarized $[1-^{13}$C]dehydroascorbate ($^{13}$C-DHA) as an MR probe to investigate redox changes in prostate cancer [49]. They compared hyperpolarized $^{13}$C-DHA MR spectroscopic signals with $^{18}$F-FDG uptake separately obtained by a small-animal PET/CT scanner [50]. Integrated PET/MR imaging will provide the accurate registration of MR redox signals and $^{18}$F-FDG uptake in the near future.

There were several limitations to the present study due to the small patient population and absence of additional experimental validation. Clinical stages, primary sites, pathological findings, and therapeutic strategies were heterogeneous. Furthermore, the usefulness of $^{62}$Cu-ATSM PET for the prognosis of HNC was not evaluated through comparisons with conventional prognostic factors such as the tumor size, advanced nodal stage, and HPV status [51, 52]. The total number of patients ($n = 30$) was not sufficient to perform multivariate tests. A larger number of patients and multi-regression analysis are required in future research. In a previous animal study, a time-dependent reversal in the intra-tumoral distribution of $^{64}$Cu-

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**Fig 8. Hypothetical relationships between excess ROS production levels, cancer cell states, and treatment options.** The arrow indicates the direction of the level of excess ROS from the normal to lethal range. The black deformed quadrangle represents excess ROS concentrations. SO: surgical operation, RT: radiation therapy, CT: chemotherapy, CR: complete response.

**Table 1.**

| Level of excess ROS | Cancer cell state               | Treatment option                           |
|--------------------|---------------------------------|--------------------------------------------|
| Lethal             | Death                           | –                                          |
| Moderate           | Aggressive, Progression         | SO / intensive RT / intensive CT           |
| – Sub-lethal       | Invasion, Metastasis            | Drugs increasing ROS production            |
|                    | Resistant to therapy            |                                            |
|                    | Worse prognosis                 |                                            |
| Low                | Indolent                        | SO / RT / CT                               |
|                    | Sensitive to therapy            | Drugs increasing ROS production            |
|                    | Better prognosis                | Antioxidants                               |
| Normal             | Second messenger                | Antioxidants (prophylactic therapy)        |
| (non-cancerous)    | Normal regulation               | when CR was achieved after treatments       |
|                    | of physiological processes      |                                            |
ATSM was reported in rats bearing homograft prostate tumors [17]. Over-reductive regions may change location in tumors according to cycling hypoxia; however, the time scale is not known. Time-dependent changes in tracer distribution need to be evaluated in humans using $^{64}$Cu-ATSM labeled with copper-64 ($t_{1/2} = 12.7$ h), allowing for longer observations. In addition, the stability of $^{62}$Cu-ATSM complexes in humans has not yet been determined. Comparisons of tumor $^{62}$Cu radioactivity in patients injected with $^{62}$Cu-ATSM and $^{62}$Cu salts ($^{62}$CuCl$_2$ or $^{62}$Cu-acetate) may be needed in order to determine whether $^{62}$Cu radioactivity in HNC is derived from the tumor uptake of intact $^{62}$Cu-ATSM complexes or cellular uptake of the ionic $^{62}$Cu radionuclide that disassociated from $^{62}$Cu-ATSM [33, 53].

Conclusions

Pretreatment $^{62}$Cu-ATSM PET provided clinically relevant information on the tumor redox status that was predictive of outcomes in patients with HNC. The high tumor uptake of $^{62}$Cu-ATSM may predict resistance to treatments and poor prognoses in patients with HNC. A reductive intensity and reductive tumor burden may both be determinants of HNC patient outcomes and potentially support optimally-individualized treatments for each patient.

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Author Contributions

Conceived and designed the experiments: TeT HK SF HO. Performed the experiments: TeT SA YS TaT. Analyzed the data: TeT SA YS HO. Contributed reagents/materials/analysis tools: MO NN TM YK. Wrote the paper: TeT AM HO.

References

1. Bhatia M, Karlenius TC, Trapani GD, Tonissen KF. Chapter 7: The interaction between redox and hypoxic signalling pathways in the dynamic oxygen environment of cancer cells. In: Tonissen K, editor. Carcinogenesis. Rijeka, Croatia: InTech; 2013. pp. 125–152.
2. Dewhirst MW, Cao Y, Moeller B. Cycling hypoxia and free radicals regulate angiogenesis and radiotherapy response. Nat Rev Cancer. 2008; 8:425–437. doi:10.1038/nrc2397 PMID: 18500244
3. Denko NC. Hypoxia, HIF1 and glucose metabolism in the solid tumour. Nat Rev Cancer. 2008; 8:705–713. doi: 10.1038/nrc2468 PMID: 19143055
4. Ishikawa K, Takenaga K, Akimoto M, Koshikawa N, Yamaguchi A, Imanishi H, et al. ROS-generating mitochondrial DNA mutations can regulate tumor cell metastasis. Science. 2008; 320:661–664. doi: 10.1126/science.1156906 PMID: 18388260
5. Sztatrowski TP, Nathan CF. Production of large amounts of hydrogen peroxide by human tumor cells. Cancer Res. 1991; 51:794–798. PMID: 1846317
6. Bai RK, Leal SM, Covarrubias D, Liu A, Wong LJ. Mitochondrial genetic background modifies breast cancer risk. Cancer Res. 2007; 67:4687–4694. PMID: 17510395
7. Nishikawa M. Reactive oxygen species in tumor metastasis. Cancer Lett. 2008; 266:53–9. doi: 10.1016/j.canlet.2008.02.031 PMID: 18362051
8. Pelicano H, Lu W, Zhou Y, Zhang W, Chen Z, Hu Y, et al. Mitochondrial dysfunction and reactive oxygen species imbalance promote breast cancer cell motility through a CXCL14-mediated mechanism. Cancer Res. 2009; 69:2375–2383. doi: 10.1158/0008-5472.CAN-08-3359 PMID: 19276362
9. Pani G, Galeotti T, Chianugi P. Metastasis: cancer cell’s escape from oxidative stress. Cancer Metastasis Rev. 2010; 29:351–378. doi: 10.1007/s10555-010-9225-4 PMID: 20366957
10. Li LZ. Imaging mitochondrial redox potential and its possible link to tumor metastatic potential. J Biorener Biomembr. 2012; 44:645–653. doi: 10.1007/s10863-012-9469-5 PMID: 22895937
11. Matsumoto K, Hyodo F, Matsumoto A, Koretsky AP, Sowers AL, Mitchell JB, et al. High-resolution mapping of tumor redox status by magnetic resonance imaging using nitroxides as redox-sensitive contrast agents. Clin Cancer Res. 2006; 12:2455–2462. PMID: 16638852

12. Cai K, Xu HN, Singh A, Moon L, Haris M, Reddy R, et al. Breast cancer redox heterogeneity detectable with chemical exchange saturation transfer (CEST) MRI. Mol Imaging Biol. 2014; 16:670–679. doi: 10.1007/s11307-014-0739-y PMID: 24811957

13. Holland JP, Lewis JS, Dehdashti F. Assessing tumor hypoxia by positron emission tomography with Cu-ATSM. J Nucl Med Imaging Biol. 2009; 53:193–200. PMID: 19293767

14. Lee ST, Scott AM. Hypoxia positron emission tomography imaging with 18F-fluoromisonidazole. Semin Nucl Med. 2007; 37:451–461. PMID: 17920352

15. Lewis JS, Sharp TL, Laforest R, Bourhis D, Palard X, Le Roux PY, et al. Prognostic value of copper-diacyl-bis(N4-methylthiosemicarbazone): effect of changes in tissue oxygenation. J Nucl Med. 2001; 42:655–661. PMID: 11337556

16. Zimny M, Gagel B, DiMartino E, Hamacher K, Coenen HH, Westhofen M, et al. FDG—a marker of tumour hypoxia? A comparison with [18F]fluoromisonidazole and pO2 polarography in metastatic head and neck cancer. Eur J Nucl Med Mol Imaging. 2006; 33:1426–1431. PMID: 16841114

17. O’Donoghue JA, Zannzonic P, Pugachev A, Wen B, Smith-Jones P, Cai S, et al. Assessment of regional tumor hypoxia using 18F-fluoromisonidazole and 64Cu(II)-diacetyl-bis(N4-methylthiosemicarbazone) positron emission tomography: Comparative study featuring microPET imaging, pO2 probe measurement, autoradiography, and fluorescent microscopy in the R3327-AT and FaDu rat tumor models. Int J Radiat Oncol Biol Phys. 2005; 61:1493–1502. PMID: 15817355

18. Carlin S, Zhang H, Reese M, Ramos NN, Chen Q, Ricketts SA. A comparison of the imaging characteristics and microregional distribution of 4 hypoxia PET tracers. J Nucl Med. 2014; 55:515–521. doi: 10.2967/jnumed.113.126615 PMID: 24491409

19. Kurthara H, Honda N, Kono Y, Arai Y. Radiolabelled agents for PET imaging of tumor hypoxia. Curr Med Chem. 2012; 19:3282–3289. PMID: 22664246

20. Fujibayashi Y, Taniuchi H, Yonekura Y, Ohtani H, Konishi J, Yokoyama A. Copper-62-ATSM: a new hypoxia imaging agent with high membrane permeability and low redox potential. J Nucl Med. 1997; 38:1155–1160. PMID: 9225812

21. Donnelly PS, Liddell JR, Lim S, Paterson BM, Cater MA, Savva MS, et al. An impaired mitochondrial electron transport chain increases retention of the hypoxia imaging agent diacyl bisc(4-methylthiosemicarbazonato)copper(II). Proc Natl Acad Sci USA. 2012; 109:47–52. doi: 10.1073/pnas.1116227108 PMID: 22173633

22. Obata A, Yoshimi E, Waki A, Lewis JS, Oyama N, Welch MJ, et al. Retention mechanism of hypoxia selective nuclear imaging/radiotherapeutic agent cu-diacetyl-bis(N4-methylthiosemicarbazone) (Cu-ATSM) in tumor cells. Ann Nucl Med. 2001; 15:499–504. PMID: 11831397

23. Ryu IS, Kim JS, Roh JL, Lee JH, Cho KJ, Choi SH, et al. Prognostic value of preoperative metabolic tumor volume and total lesion glycolysis measured by 18F-FDG PET/CT in salivary gland carcinomas. J Nucl Med. 2013; 54:1032–1038. doi: 10.2967/jnumed.112.116053 PMID: 23670902

24. Abgral R, Keromnes N, Robin P, Le Roux PY, Bourhis D, Paillard X, et al. Prognostic value of volumetric parameters measured by 18F-FDG PET/CT in patients with head and neck squamous cell carcinoma. Eur J Nucl Med Mol Imaging. 2014; 41:659–667. doi: 10.1007/s00259-013-2618-1 PMID: 24196922

25. Pak K, Cheon GJ, Nam HY, Kim SJ, Kang KW, Chung JK, et al. Prognostic Value of metabolic tumor volume and total lesion glycolysis in head and neck cancer: A systematic review and meta-analysis. J Nucl Med. 2014; 55:884–890. doi: 10.2967/jnumed.113.133801 PMID: 24752671

26. Sato Y, Tsujikawa T, Oh M, Mori T, Kiyono Y, Fujieda S, et al. Assessing tumor hypoxia in head and neck cancer by PET with 62Cu-diacyl-bis(N4-methylthiosemicarbazone). Clin Nucl Med. 2014; 39:1027–1032. doi: 10.1097/RLU.0000000000000537 PMID: 25140555

27. Kostiawanaranker A, Oh M, Kudo T, Kiyono Y, Mori T, Kimura Y, et al. Different distribution of 62Cu ATSM and 18F-FDG in head and neck cancers. Clin Nucl Med. 2012; 37:252–257. doi: 10.1097/RLU.0b013e31823eaadb PMID: 22310251

28. Lohith TG, Kudo T, Demura Y, Umeda Y, Kiyono Y, Fujibayashi Y, et al. Pathophysiologic correlation between 62Cu-ATSM and 18F-FDG in lung cancer. J Nucl Med. 2009; 50:1948–1953. doi: 10.2967/jnumed.109.069021 PMID: 19910425

29. Miller TR, Grigsby PW. Measurement of tumor volume by PET to evaluate prognosis in patients with advanced cervical cancer treated by radiation therapy. Int J Radiat Oncol Biol Phys. 2002; 53:353–359. PMID: 12023139
30. DeLong ER, DeLong DM, Clarke-Pearson DL. Comparing the areas under two or more correlated receiver operating characteristic curves: a nonparametric approach. Biometrics. 1988; 44:837–845. PMID: 3203132

31. Yoshii Y, Furukawa T, Kiyono Y, Watanabe R, Waki A, Mori T, et al. Copper-64-diacetyl-bis(N4-methylthiosemicarbazone) PET imaging to predict highly malignant tumor grades and hypoxia-inducible factor-1α expression in patients with glioma. AJNR Am J Neuroradiol. 2013; 34:92–99. doi: 10.3174/ajnr.A3159 PMID: 22700754

32. Bowen SR, van der Kogel AJ, Nordsmark M, Bentzen SM, Jeraj R. Characterization of positron emission tomography hypoxia tracer uptake and tissue oxygenation via electrochemical modeling. Nucl Med Biol. 2011; 38:771–780. doi: 10.1016/j.nucmedbio.2011.02.002 PMID: 21843774

33. Dietz DW, Dehdashi F, Grigsby PW, Malyapa RS, Picus J, et al. Tumor hypoxia detected by positron emission tomography with 60Cu-ATSM as a predictor of response and survival in patients undergoing neoadjuvant chemoradiotherapy for rectal carcinoma: a pilot study. Dis Colon Rectum. 2008; 51:1641–1648. doi: 10.1007/s10350-008-9420-3 PMID: 18682861

34. Dehdashi F, Grigsby PW, Lewis JS, Laforest R, Siegel BA, Welch MJ. Assessing tumor hypoxia in cervical cancer by PET with 60Cu-labeled diacetyl-bis(N4-methylthiosemicarbazone). J Nucl Med 2008; 49:201–205. doi: 10.2967/jnumed.113.119917 PMID: 24337603

35. Dehdashi F, Grigsby PW, Mintun MA, Lewis JS, Siegel BA, Welch MJ. Assessing tumor hypoxia in cervical cancer by positron emission tomography with 60Cu-ATSM: relationship to therapeutic response—a preliminary report. Int J Radiat Oncol Biol Phys. 2003; 55:1233–1238. PMID: 12544532

36. Dietz DW, Dehdashi F, Grigsby PW, Malyapa RS, Myerson RJ, Picus J, et al. Tumor hypoxia detected by positron emission tomography with 60Cu-ATSM as a predictor of response and survival in patients undergoing neoadjuvant chemoradiotherapy for rectal carcinoma: a pilot study. Dis Colon Rectum. 2008; 51:1641–1648. doi: 10.1007/s10350-008-9420-3 PMID: 18682861

37. Tateishi K, Tateishi U, Nakanowatari S, Ohtake M, Minamimoto R, Suenaga J, et al. Application of 62Cu-diacetyl-bis(N4-methylthiosemicarbazone) PET imaging to predict highly malignant tumor grades and hypoxia-inducible factor-1α expression in patients with glioma. AJNR Am J Neuroradiol. 2013; 34:92–99. doi: 10.3174/ajnr.A3159 PMID: 22700754

38. Tateishi K, Tateishi U, Sato M, Yamanaka S, Kanno H, Murata H, et al. Application of 62Cu-diacetyl-bis(N4-methylthiosemicarbazone) PET imaging to predict highly malignant tumor grades and hypoxia-inducible factor-1α expression in patients with glioma. AJNR Am J Neuroradiol. 2013; 34:278–284. doi: 10.3174/ajnr.A3679 PMID: 23928140

39. Chao KS, Bosch WR, Multic S, Lewis JS, Dehdashi F, Mintun MA, et al. A novel approach to overcome hypoxic tumor resistance: Cu-ATSM-guided intensity-modulated radiation therapy. Int J Radiat Oncol Biol Phys. 2001; 49:1171–1182. PMID: 11240261

40. Bowen SR, Flynn RT, Bentzen SM, Jeraj R. On the sensitivity of IMRT dose optimization to the mathematical form of a biological imaging-based prescription function. Phys Med Biol. 2009; 54:1483–1501. doi: 10.1088/0031-9155/54/6/007 PMID: 19218733

41. Gornini C, Hamis IS, Mak TW. Modulation of oxidative stress as an anticancer strategy. Nat Rev Drug Discov. 2013; 12:951–974. doi: 10.1038/nrd4002 PMID: 24287781

42. Nogueira V, Hay N. Molecular pathways: reactive oxygen species homeostasis in cancer cells and implications for cancer therapy. Clin Cancer Res. 2013; 19:4309–4314. doi: 10.1158/1078-0432.CCR-12-1424 PMID: 23719265

43. Acharya A, Das I, Chandhok D, Saha T. Redox regulation in cancer: a double-edged sword with therapeutic potential. Oxid Med Cell Longev. 2010; 3:284. doi: 10.4161/oxim.3.1.10095 PMID: 20416222

44. Goh J, Enns L, Fatemie S, Hopkins H, Morton J, Pettan-Brewer C, et al. Mitochondrial targeted catalase suppresses invasive breast cancer in mice. BMC Cancer. 2011; 11:191. doi: 10.1186/1471-2407-11-191 PMID: 21605372

45. Greenlee H, Kwan ML, Kushi LH, Song J, Castillo A, Weltzien E, et al. Antioxidant supplement use after breast cancer diagnosis and mortality in the Life After Cancer Epidemiology (LACE) cohort. Cancer. 2012; 118:2048–2058. doi: 10.1002/cncr.26526 PMID: 21953120

46. Harris HR, Orsini N, Wool A. Vitamin C and survival among women with breast cancer: a meta-analysis. Eur J Cancer. 2014; 50:1223–1231. doi: 10.1016/j.ejca.2014.02.013 PMID: 24613622

47. Mazdak H, Zia H. Vitamin E reduces superficial bladder cancer recurrence: a randomized controlled trial. Int J Prev Med. 2012; 3:110–115. PMID: 22347607

48. Bairati I, Meyer F, Gélinas M, Fortin A, Nabid A, Brochet F, et al. A randomized trial of antioxidant vitamin C plus ascorbate as an endogenous redox sensor for in vivo metabolic imaging. Proc Natl Acad Sci U S A. 2011; 108:18606–18611. doi: 10.1073/pnas.1106920108 PMID: 22042839
50.  Keshari KR, Sai V, Wang ZJ, Vanbrocklin HF, Kurhanewicz J, Wilson DM. Hyperpolarized [1\textsuperscript{3}C]dehydroascorbate MR spectroscopy in a murine model of prostate cancer: comparison with \textsuperscript{18}F-FDG PET. J Nucl Med. 2013; 54:922–928. doi:10.2967/jnumed.112.115402 PMID: 23575993

51.  Brockstein B, Haraf DJ, Rademaker AW, Kies MS, Stenson KM, Rosen F, et al. Patterns of failure, prognostic factors and survival in locoregionally advanced head and neck cancer treated with concomitant chemoradiotherapy: a 9-year, 337-patient, multi-institutional experience. Ann Oncol. 2004; 15:1179–1186. PMID: 15277256

52.  O’Sullivan B, Huang SH, Siu LL, Waldron J, Zhao H, Perez-Ordonez B, et al. Deintensification candidate subgroups in human papillomavirus-related oropharyngeal cancer according to minimal risk of distant metastasis. J Clin Oncol. 2013; 31:543–550. doi:10.1200/JCO.2012.44.0164 PMID: 23295795

53.  Jørgensen JT, Persson M, Madsen J, Kjaer A. High tumor uptake of \textsuperscript{64}Cu: implications for molecular imaging of tumor characteristics with copper-based PET tracers. Nucl Med Biol. 2013; 40:345–350. doi:10.1016/j.nucmedbio.2013.01.002 PMID: 23394821