Differential Diagnosis of Axillary Inflammatory and Metastatic Lymph Nodes in Rabbit Models by Using Diffusion-Weighted Imaging: Compared with Conventional Magnetic Resonance Imaging

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Objective: This experiment aims to determine the diagnostic value of diffusion-weighted imaging (DWI) in the differentiation of axillary inflammatory lymph nodes from metastatic lymph nodes in rabbit models in comparison with conventional magnetic resonance imaging (MRI).

Materials and Methods: Conventional MRI and DWI were performed at 4 weeks after successful inoculation into the forty female New Zealand white rabbits’ mammary glands. The size-based and signal-intensity-based criteria and the relative apparent diffusion coefficient (rADC) value were compared between the axillary inflammatory lymph nodes and metastatic lymph nodes, with histopathological findings as the reference standard. Receiver operating characteristic (ROC) curve analysis was performed to evaluate the diagnostic performance of the aforementioned criteria and rADC value in differentiating the axillary inflammatory lymph nodes from metastatic lymph nodes.

Results: Thirty-two axillary inflammatory lymph nodes and 46 metastatic ones were successfully isolated and taken into pathological analysis. The differences of the aforementioned criteria between the two groups were not statistically significant (p > 0.05). However, the rADC value of the inflammatory lymph nodes (0.9 ± 0.14) was higher than that of metastatic ones (0.7 ± 0.18), with significant difference (p = 0.016). When the rADC value was chosen as 0.80, the area under the ROC curve is greater than all other criteria, and the sensitivity, specificity, accuracy, positive predictive value, and negative predictive value for differentiating two groups were 86.2%, 79.3%, 81.2%, 84.2%, and 85.6%, respectively.

Conclusion: Diffusion-weighted imaging is a promising new technique for differentiating axillary inflammatory lymph nodes from metastatic lymph nodes. Compared with routine magnetic resonance sequences, DWI could provide more useful physiological and functional information for diagnosis.

Index terms: Axillary lymph node; Diffusion-weighted imaging; Relative ADC; Animal model

INTRODUCTION

Axillary lymph node involvement is the most common route of breast cancer metastases, and is an essential prognostic factor and an important determinant in the treatment of patients with breast cancer (1-4). Axillary lymph nodes dissection with histopathological examination of the surgical specimen is regarded as the gold standard for detecting involvement of the lymph nodes (1, 2). Complications, such as seroma formation, numbness, limitation of shoulder movement, and lymphedema, have...
been reported (5-7). Thus, a noninvasive technique that assists in the accurate identification of axillary lymph node metastases before operation would be beneficial by helping surgeons to choose appropriate treatment regimens to improve the clinical outcome and minimize complications associated with unnecessary lymphadenectomy.

With magnetic resonance imaging (MRI), computed tomography, and ultrasonography techniques, the preoperative assessment of axillary lymph node status is based mainly on measurement of nodal dimensions, such as maximum long-axis diameter, short-axis diameter or long/short-axis ratio, but these techniques are somewhat limited. In addition, morphologic criteria (e.g., shape, thickened lobular cortex, displacement and/or absence of fatty hilus), enhancement patterns, and grouping of lymph nodes are further important parameters (8-11). All these criteria remain controversial, and recommendations for differentiation between metastatic and non-metastatic lymph node vary widely.

Diffusion-weighted imaging (DWI) facilitates the noninvasive characterization of various tissues on the basis of their water diffusion properties. Any architectural changes in the proportion of extracellular to intracellular water protons will alter the diffusion coefficient of the tissue (12-15), thus providing information about the biophysical properties of tissues in vivo. Quantitative measurement of apparent diffusion coefficient (ADC) could reflect the degree of restriction of diffusion of different tissues. Although accumulating evidence indicated that the ADC value may improve the accuracy for diagnosing metastatic lymph nodes in uterine cervical cancer and head and neck cancer (16-20). However, whether ADC value is potentially useful in detecting axillary metastatic lymph nodes is less clear. There has only been one report evaluating axillary lymph nodes by diffusion-weighted MRI in patient with breast cancer: the results of which concluded that the differences in the ADC value between metastatic and non-metastatic nodes were not significant (21). In clinical studies, DWI may find numerous lymph nodes, although for the most part it is extremely difficult to produce accurate pathology results from images for each lymph node, one by one. We performed our present study in order to have the exact pathological result for a lymph node, and the purpose of this experiment was to investigate the feasibility of DWI technique to discriminate between axillary inflammatory and metastatic lymph nodes in rabbit models.

**MATERIALS AND METHODS**

**Animal Model Preparation**

This experiment was approved by the animal care committee at Tianjin Medical University General Hospital. Forty healthy female New Zealand white rabbits offered by the Laboratory Animal Center of Tianjin Medical University (weighing 2.0-2.5 kg) were randomly divided into two equal groups. The rabbits were allowed food and water ad libitum. After the rabbits were anesthetized, by injecting 3% soluble pentobarbital into the abdominal cavity at a dose of 1 mL/kg, 0.5 mL Complete Freund’s adjuvant (brought from Sigma Corporation, St. Louis, MO, USA) was injected into the rabbits’ mammary glands underneath the lateral upper quadrant of the bilateral second nipple so as to set up the axillary inflammatory reactive hyperplastic lymph node models, and 1 mL VX2 tumor tissue suspension (provided by Pathology faculty of China Xiehe Medical University) was inoculated into another group of rabbits into the same location as that of the axillary metastatic lymph node models described previously (22). The rabbits were sacrificed immediately after MRI examination and imaging and histopathological comparisons were conducted.

**MRI Scanning Protocol and Parameters**

All MRI examinations were performed with a 1.5 T superconducting magnet (Twinspeed Infinity with Excite II, GE Medical Systems, Milwaukee, WI, USA) and a knee coil to improve the resolution. MRI covered bilateral axillary fossa areas were acquired 4 weeks after inoculation for the axillary inflammatory and metastatic lymph node. The anesthetic regimen used for implantations were also used for MRI examination. All of the animals were imaged in the prone position with elevated arms. Prior to DWI, axial and sagittal T2WI, fast spin-echo sequences with or without fat suppression (TR/TE, 3500/68 msec; slice thickness, 3 mm; interslice gap, 0.5 mm; field of view, 15 x 15 cm; matrix, 256 x 224; number of excitation, 4; echo train length, 15); and axial and sagittal T1WI spin-echo sequences with or without fat suppression (TR/TE, 520/11 msec; matrix, 256 x 160, the remaining parameters were the same as those of T2WI) were obtained. Transverse DWI were obtained using array spatial sensitivity encoding technique (ASSET) and free-breathing short TI inversion recovery single-shot echoplanar-imaging (STIR-SS-EPI) sequence with the following parameters (TR/TE, 5000/67.3 msec; slice thickness, 3 mm; interslice gap, 0.5 mm; field of view, 15 x 15 cm; matrix,
128 x 128; number of excitation, 4, parallel factor, 2) with b values of 0 and 800 s/mm². The DWI gradients were applied in all three orthogonal directions, which coincided with the slice-selective, phase-encoding, and readout directions. The scanning time of all sequences was less than 25 minutes.

Measurements on MRI and Image Analysis

All MRI were assessed with an emphasis placed on the bilateral axillary fossa lymph nodes. Two experienced radiologists, who were blinded to the histological findings, evaluated all the MRI by consensus. Both the axillary inflammatory or metastatic lymph nodes with the short-axis diameter equal or greater than 5 mm were included in our study. The long-axis (L) and short-axis diameter (S) were measured on the corresponding maximum section of each lymph node on axial T2WI, respectively, and the long/short-axis ratio (L/S) was calculated. The signal intensity on T2WI and DWI (S\text{T2WI}, S\text{DWI}) of each selected lymph node was measured. The ADC maps were calculated on a pixel-by-pixel basis by using built-in software (AW4.2 Functool; GE Healthcare, Milwaukee, WI, USA). We used the corresponding central slice of each lymph node on the ADC map, a round or elliptical region of interest (ROI) covering about 3/4 of the entire area of the selected lymph node attempting to avoid inclusion of the margins; while T2W imaging was used as the anatomical reference. The relative ADC (rADC) value was calculated by ADC\text{lymph node}/ADC\text{reference site}, and the dorsal muscle was determined to be the reference site for the rADC. The ROI with the same size was also drawn on the center area of the ipsilateral dorsal muscle at the same level of each lymph node on the ADC map. The area of the ROI in the selected axillary lymph nodes was 25-150 mm², according to their different sizes. All the values were averaged from three-time measurements and expressed as the mean ± standard deviation.

Statistical Analysis

Statistical analyses were performed by using Statistical Product and Service Solutions (SPSS, version 18.0, Chicago, IL, USA). All the measurements were in normal distribution. Differences of L, S, L/S, signal intensity on T2WI (S\text{T2WI}), signal intensity on DWI (S\text{DWI}), and the rADC value between the axillary pathologically proven inflammatory lymph nodes and the malignant lymph nodes were compared respectively, using independent t test with a level of p value less than 0.05 considered statistically significant. A receiver operating characteristic (ROC) curve analysis was used to compare the diagnostic performance of rADC value and each of the size-based criteria and signal-intensity-based criteria for the differentiation of the axillary inflammatory and metastatic lymph nodes. Thereafter, the appropriate areas under the curve were evaluated and compared. From the ROC curve analysis, The Youden’s index was used in determining the optimal threshold rADC value for differentiating axillary inflammatory from metastatic lymph nodes. Once the optimal criterion was obtained, we would calculate the sensitivity, specificity, accuracy, and positive and negative predictive values (PPV, NPV) using the corresponding resulting threshold.

RESULTS

Pathological Results

According to the MRI, a total of 78 lymph nodes in bilateral axillary fossa with a short-axis diameter equal to or larger than 5 mm, including 32 inflammatory and 46 metastatic ones, were successfully isolated and taken into analysis. The inflammatory lymph nodes had smooth pinkish-grey surfaces, while the metastatic lymph nodes had shaggy pale-grey surfaces with a fish like texture (Fig. 1). Light microscopy showed inflammatory lymph nodes with abundant lymphocytes and plasmacytes infiltration, reactive hyperplasia, and fibrous connective tissue proliferation (Fig. 1). Histopathologic analysis of the metastatic lymph nodes revealed that nest-like gathered tumor cells with enlarged irregular nuclei or pathological mitotic figures, plasma cells, and (rarely) lymphocytes were observed in the nodes (Fig. 1).

Image Characteristics of the Two Group Lymph Nodes

When ASSET and STIR were used, image distortion was significantly reduced to a minimum, and DWI was of diagnostic quality in all cases; no cases were excluded from our study. All of the axillary inflammatory and metastatic lymph nodes were isointense on T1WI, hyperintense relative to that of adjacent skeletal muscle on T2WI and DWI, and all of the signal intensity of the selected lymph nodes was homogeneous without visible necrosis and cystic degeneration. On pseudo-color ADC maps, the inflammatory lymph nodes showed as green or yellow regions (Fig. 2), while the metastatic ones manifested as blue regions (Fig. 3).
Comparison of Size-Based Criteria, Signal-Intensity-Based Criteria, and rADC Value between the Two Group Lymph Nodes

The mean value of L, S, L/S, $S_{T2WI}$, $S_{DWI}$, and rADC of the axillary inflammatory and metastatic lymph nodes were 10.21 ± 0.24 mm, 5.00 ± 0.25 mm, 1.98 ± 0.13 mm, 380.25 ± 28.45 mm, 878.64 ± 51.38 mm, and 0.9 ± 0.14 mm and 13.72 ± 0.19 mm, 8.77 ± 0.32 mm, 1.49 ± 0.15 mm, 452.11 ± 60.78 mm, 975.44 ± 33.62 mm, and 0.7 ± 0.18 mm, respectively. Each of the size-based criteria and signal-intensity-based criteria between two groups showed no statistically significant difference; however, the rADC value of the inflammatory lymph nodes was higher than that of metastatic ones in axillary fossa (0.9 ± 0.14 mm vs. 0.7 ± 0.18 mm) with $b$ values of 0 and 800 s/mm$^2$: the difference between the two groups was statistically significant (Table 1).

The appropriate area under the ROC curve for L, S, L/S, $S_{T2WI}$, $S_{DWI}$, and rADC value was 0.67, 0.70, 0.57, 0.49, 0.38, and 0.82, respectively (Fig. 4). Since the area for the rADC value was greater than those of all other criteria, the former was used as the representative index for differentiation of inflammatory from metastatic lymph nodes. When choosing 0.80 as diagnostic optimal threshold of the rADC value, the Youden index was the maximum, and its sensitivity, specificity, accuracy, PPV, and NPV was 86.2%, 79.3%, 81.2%, 84.2%, and 85.6%, respectively.

**DISCUSSION**

A noninvasive technique that accurately assesses lymph node metastasis would be of great benefit to patients with breast cancer, since surgical lymph node dissection, which is regarded as the gold standard method for the diagnosis of lymph node metastasis, will increase the cost and time...
of diagnosis and the risk of complications to the patient (4, 6). Therefore, if we were able to determine preoperatively whether metastases to the axillary lymph nodes were present or not, we would be able to avoid unnecessary lymphadenectomy and, meanwhile, improve treatment management and minimize the surgical complications and costs. Traditional size criteria indicated that nodes with short-axis diameter of longer than 10 mm were defined as metastasis (23, 24). However, investigators have proven that this criteria is inaccurate (3, 4), and based on the size criteria, the sensitivity in the diagnosis of metastatic nodes is low (53-62%) (25). Moreover, Obwegeser et al. (26) reported that, in histological analysis of 1249 axillary lymph nodes in 71 patients with breast cancer, 13.7% of metastatic nodes were 5-9 mm in short-axis diameter. In our study, there was no statistical difference between L, S, and L/S between the axillary inflammatory and metastatic lymph nodes, respectively, and neither was the signal intensity on T2WI, in agreement with the results obtained by Som (27).

DWI, which is noninvasive, does not require contrast medium administration, and it does not involve ionizing radiation, an important MRI technique that enables the radiologist to move from morphological to functional

Fig. 2. Appearance of conventional MRI, diffusion-weighted imaging and apparent diffusion coefficient map of axillary inflammatory lymph node.
Inflammatory lymph node in right axillary fossa on axial T2WI shows iso-intensity with unclear borderline (arrow) (A). Axial T2WI shows high signal intensity (arrow) (B). Corresponding diffusion-weight imaging demonstrates homogeneous high signal intensity (arrow), and conspicuity in identification of same node is higher in this image compared with T2WI (C). Node is depicted as area of green in most part, with scattered yellow dots (arrow) on pseudo-color apparent diffusion coefficient map, and relative apparent diffusion coefficient value of this node is 0.86 (D).
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Assessment of diseases. The conspicuity in the identification of nodes on DWI was significantly higher than that on T2WI, since the axillary lymph nodes were shown with marked high signal intensities in comparison with the adjacent muscle and surrounding normal vessels on DWI that made it easy to identify (28). However, visual assessment of DWI to differentiate the axillary inflammatory from metastatic lymph nodes was a rather difficult task, as shown in Figure 2 and 3, because both group lymph nodes showed high signal intensities on DWI. In contrast, the ADC values calculated from DWI can provide quantitative analysis of microscopic water diffusivity in the target tissues and can completely exclude the T2 shine-through effect (29).

In biological tissue, the ADC values are considered to be mainly influenced by the motion of water molecules in the extracellular space and capillary perfusion. Generally, the larger the b-value is, the greater the degree of signal attenuation from the motion of water molecules is (29, 30). In our study, DWI was performed with a high b-value of 800 s/mm², which could evaluate water diffusion more precisely and nearly rule out the effects of capillary perfusion.

The lower ADC value always observed in metastatic lymph nodes could be explained by the histopathological manifestation of the resected specimen. In our study, the VX2 tumor is an anaplastic squamous cell carcinoma and axillary metastatic lymph nodes are replaced by cancer cells, resulting in high cell density and enlarged cell size, which would reduce extracellular spaces; meanwhile, the cancer cells had more organelle, enlarged nuclei, hyperchromatism, and high nuclear-to-cytoplasmic ratio, limiting the diffusion of water molecules in intracellular spaces. These histopathological characteristics resulted in a decrease in the ADC value.

Although many studies have proven the feasibility of ADC for cancer detection in various organs by showing a lower ADC in cancer tissue than in non-cancerous tissue, the mean ADC in each cancer seems to vary greatly according to the studies. For example, the mean ADC of breast cancer ranged from 0.75 x 10⁻³ mm²/sec to 1.50 x 10⁻³ mm²/sec in previous studies (31-34).

**Table 1. Comparison of L, S, L/S, SI T2WI, and SI DWI between Group Lymph Nodes**

| Measurements | Inflammatory Lymph Nodes (n = 32) | Metastatic Lymph Nodes (n = 46) | t    | P   |
|--------------|----------------------------------|--------------------------------|------|-----|
| L (mm)       | 10.2 ± 0.24                      | 13.7 ± 0.19                    | -1.305 | 0.128|
| S (mm)       | 5.0 ± 0.25                       | 8.8 ± 0.32                     | -1.962 | 0.079|
| L/S          | 2.0 ± 0.13                       | 1.5 ± 0.15                     | 1.107  | 0.209|
| SI T2WI      | 380.3 ± 28.45                    | 452.1 ± 60.78                  | -0.967 | 0.312|
| SI DWI       | 878.6 ± 51.38                    | 975.4 ± 33.62                  | -0.741 | 0.464|
| rADC value   | 0.9 ± 0.14                       | 0.7 ± 0.18                     | 4.879  | 0.016|

**Note.**—L = long-axis diameter, L/S = long/short-axis ratio, S = short-axis diameter, SI T2WI = signal intensity on T2WI, rADC = relative apparent diffusion coefficient

**Fig. 3. Manifestation of diffusion-weighted imaging and apparent diffusion coefficient map of axillary metastatic lymph nodes.**

Two axillary metastatic lymph nodes in bilateral axillary fossa on axial diffusion-weighted imaging show obviously homogeneous high signal intensity with clear margin (arrow) **(A)**. Both of them demonstrated as areas of blue on corresponding apparent diffusion coefficient map (arrow), and relative apparent diffusion coefficient value of left and right nodes is 0.80, 0.55, respectively **(B)**.

Please note that the table and figures are not included in the natural text. The provided text focuses on the assessment of diseases using DWI and ADC values, highlighting the differences between inflammatory and metastatic lymph nodes.
There may be two explanations for this variance. First, ADC is variable according to various factors, such as magnetic resonance (MR) acquisition parameters, magnetic field, location and area of ROI, patient age, and body temperature (35, 36). Park et al. (17) suggested that normalization of ADC may reduce this instability of ADC, known as rADC, which is calculated by the formula ADC\text{lesion} / ADC\text{reference site}, and their results show that the renal cortex is an appropriate reference site for rADC, and that rADC may improve the accuracy for diagnosing metastatic lymph nodes in uterine cervical cancer. Lin et al. (19) also showed significant differences of rADC between metastatic and non-metastatic lymph nodes that showed no difference in ADC.

In our experiment, the coverage of MR examination did not reach the rabbits' kidneys. We presumed that muscle tissue was most extensively distributed in animals' bodies, and the muscle was more generally used as the reference site of rADC value. We used the ipsilateral dorsal muscle of the rabbits in our study at the same level of each lymph node as the reference site of rADC, playing the role of normalization. Generally, the dorsal muscle tissue of rabbits is not vulnerable to injured, and the ADC value is relatively steady. Moreover, axillary lymph nodes and the ipsilateral dorsal muscle are almost located in the same phase-encoding direction. The possible phase-encoding artifacts can be avoided by dividing between them. Our results showed that the rADC value of the axillary inflammatory lymph nodes (0.9 ± 0.14) was higher than that of metastatic ones (0.7 ± 0.18) with significant difference (t = 4.879; \( p = 0.016 \)), but there was a little overlap between the two groups. When the rADC value chosen as the best performing cutoff was 0.80 (AUC = 0.822), the sensitivity, specificity, accuracy, PPV and NPV of rADC value in differentiating lymph nodes of the two group was 86.2%, 79.3%, 81.2%, 84.2%, and 85.6%, respectively, all greater than that of all size-based criteria of other reports (24, 25). Maybe there were two plausible explanations for this overlap. We found that not all metastatic lymph nodes were entirely replaced by cancer cells; some of them were partially replaced by cancer cells, resulting in metastatic areas with lower ADC and non-metastatic areas with higher ADC, and the ADC value within a lymph node is rather heterogeneous, containing areas of both metastatic and non-metastatic portions. In contrast, in inflammatory lymph nodes, inflammatory cell infiltration, reactive hyperplasia, and fibrous connective tissue proliferation could be seen, which also would limit the diffusion of water molecules, resulting in a decrease in ADC value. ADC has an inherent limitation for differentiating inflammatory lymph nodes from metastatic lymph nodes because ADC is not specific for cancer cells but only reflects tissue diffusivity. Although tissue diffusivity may differ between inflammatory and metastatic lymph nodes, there must be an overlap, as various conditions, such as ischemia and inflammation, also reduce ADC. This overlap cannot be solved by rADC.

This study has several limitations. First, only axillary lymph nodes that had short-axis diameters equal or greater than 5 mm on T2WI were analyzed, the ability of DWI in detecting lymph nodes smaller than 5 mm in short-axis diameter was uncertain, and the ADC measurements on those small nodes would be hampered because of relatively low spatial resolution and signal-to-noise ratio. Second, we did not use a combined evaluation of the rADC value and size-based criteria, which may improve the accuracy of detection of lymph node metastasis further. Third, the animal model in this study is made with VX2 carcinoma, which is a squamous epithelium testicular cancer. Primary breast cancers usually are a kind of adenocarcinoma, and the behavior of metastasis could be different from that of squamous cell cancer, which could lower the clinical implications of this study.

In conclusion, quantitative measurement of rADC values...
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had higher accuracy for differentiating axillary inflammatory from metastatic lymph nodes. DWI should be applied in the clinical area owing to its relatively short acquisition time and lack need for the administration of exogenous contrast medium.

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