The neglected role of abdominal compliance in organ-organ interactions

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Abstract
This article is one of ten reviews selected from the Annual Update in Intensive Care and Emergency Medicine 2016. Other selected articles can be found online at http://www.biomedcentral.com/collections/annualupdate2016. Further information about the Annual Update in Intensive Care and Emergency Medicine is available from http://www.springer.com/series/8901.

Background
Over the last few decades, increasing attention has been given to understanding the pathophysiology, etiology, prognosis, and treatment of elevated intra-abdominal pressure (IAP) in trauma, surgical, and medical patients. However, there is still a relatively poor understanding of intra-abdominal volume (IAV) and the relationship between IAV and IAP (i.e., abdominal compliance \( C_{ab} \)). According to the consensus definitions proposed by the World Society on Abdominal Compartment Syndrome (WSACS), \( C_{ab} \) is defined as a measure of the ease of abdominal expansion, determined by the elasticity of the abdominal wall and diaphragm [1]. \( C_{ab} \) should be expressed as the change in IAV per change in IAP (expressed in ml/mmHg). \( C_{ab} \) is one of the most neglected parameters in critically ill patients, despite playing a key role in understanding the deleterious effects of unadapted IAV on IAP, organ-organ interactions and end-organ perfusion [2, 3]. Although there are some papers related to \( C_{ab} \) in surgical patients, only a few papers have been published addressing this issue in critically ill patients [2–4].

Definitions
The abdominal compartment
The abdominal compartment is a technical masterpiece as this small human cavity houses 8.5 m of intestine. Analogous to the skull, the abdomen can be considered as a relatively closed box with an anchorage above (costal arch) and rigid (spine and pelvis) or partially flexible walls (abdominal wall and diaphragm) filled with solid organs and hollow viscera [2]. The size and/or volume of the abdomen may be affected by the varying location of the diaphragm, the shifting position of the costal arch, the contractions of the abdominal wall, and the contents contained within the intestines.

The abdominal wall
The abdominal wall represents the boundaries of the abdominal cavity between the xyphoid bone and costal margins cranially and the iliac and pubic bones of the pelvis caudally. \( C_{ab} \) is mainly defined by the elasticity of the different muscle layers of the abdominal wall (anterior and lateral parts) and to a lesser extent the diaphragm muscle.

Intra-abdominal pressure and abdominal hypertension
Intra-abdominal pressure
The IAP is the steady-state pressure concealed within the abdominal cavity. The reference standard for intermittent IAP measurements is via the bladder. IAP should be expressed in mmHg and measured at the end of exhalation in the supine position after ensuring that abdominal muscle contractions are absent and with the transducer zeroed at the level where the midaxillary line crosses the iliac crest [1].

Baseline IAP
Also called resting, starting, static or opening IAP during laparoscopy, the baseline IAP is the IAP obtained at normal resting conditions [2]. Normal IAP is considered as 5–7 mmHg in healthy individuals, and approximately 10 mmHg in critically ill adults [5].

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**Intra-abdominal hypertension (IAH)**

IAH is defined as a sustained or repeated pathological elevation in IAP ≥ 12 mmHg. IAH is graded as follows: Grade I, IAP 12–15 mmHg; Grade II, IAP 16–20 mmHg; Grade III, IAP 21–25 mmHg; and Grade IV, IAP > 25 mmHg [1].

**Abdominal compartment syndrome (ACS)**

ACS is defined as a sustained IAP > 20 mmHg (with or without an abdominal perfusion pressure [APP] < 60 mmHg) that is associated with new organ dysfunction/failure. In contrast to IAH, ACS is an all-or-nothing phenomenon [1].

**Delta IAP**

ΔIAP is calculated as the difference between the end-inspiratory (IAP_{ei}) and the end-expiratory (IAP_{ee}) IAP value. The higher the ΔIAP, the lower the C_{ab}.

\[ ΔIAP = IAP_{ei} - IAP_{ee} \]

**Abdominal pressure variation (APV)**

APV is calculated as the difference between the IAP_{ei} and the IAP_{ee} value, or ΔIAP, divided by the mean IAP and is expressed as a percentage. The higher the APV, the lower the C_{ab}.

\[ APV = \frac{ΔIAP}{mean IAP} = \frac{IAP_{ei} - IAP_{ee}}{mean IAP} \]

**Intra-abdominal volume**

**Baseline IAV**

Also called resting, starting or static IAV, the baseline IAV is the IAV at baseline conditions without additional pathologic volume increase or C_{ab} decrease, with corresponding baseline IAP. The baseline IAV in healthy individuals is around 13 l [2].

**Abdominal distension**

This is defined as a sagittal abdominal diameter (approximately at the level of the umbilicus) higher than the virtual line between the xiphoid and symphysis pubis.

**Abdominal workspace**

This is the additional IAV that can be added to the baseline IAV when IAP is limited to a certain pressure (e.g., 14 mmHg) during laparoscopic surgery. The normal workspace during laparoscopy ranges between 3 and 6 l.

**Maximal stretched volume**

The maximal volume is calculated as the baseline IAV + the maximal workspace resulting in maximal stretch of the abdominal cavity (from ellipse to sphere on a transverse plane). The maximal stretched volume depends on baseline IAP and C_{ab}.

**Abdominal compliance**

**Abdominal compliance**

C_{ab} is defined as the ease with which abdominal expansion can occur, and is determined by the elasticity of the abdominal wall and diaphragm. Increased compliance indicates a loss of elastic recoil of the abdominal wall. Decreased compliance means that the same change in IAV will result in a greater change in IAP. It should be expressed as the change in IAV per change in IAP (ml/mmHg) [1]. Normal C_{ab} is around 250 to 450 ml/mmHg.

**Abdominal PV relationship**

Importantly, C_{ab} is measured differently than IAP, it is only a part of the total abdominal pressure-volume (PV) relationship.

\[ Compliance (C) = \frac{ΔV}{ΔP} \text{ or thus } C_{ab} = \frac{ΔIAV}{ΔIAP} \]

\[ Elastance (E) = \frac{ΔP}{ΔV} = \frac{1}{C} \text{ or thus } E_{ab} = \frac{ΔIAP}{ΔIAV} \]

The relationship between IAV and IAP is curvilinear with an initial linear part followed by an exponential increase once a critical volume is reached (Fig. 1).

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**Fig. 1 Pressure-volume curve in the abdominal compartment.**

Abdominal pressure-volume curves in a patient with low abdominal compliance (square) and normal compliance (circles). At a baseline IAV of 4 l, the same 2 l increase in IAV will only lead to a small increase in IAP (5 mmHg) in a patient with good abdominal compliance versus a high increase in IAP (15 mmHg) in the case of a stiff abdominal wall and diaphragm. The compliance is 133 ml/mmHg [2000/(37 − 22)] versus 400 ml/mmHg [2000/(12 − 7)] for the same change in IAV from 4 to 6 l. Adapted from [2] with permission.
Pathophysiology

Accommodation of the abdominal cavity

In contrast to the intracranial compartment that is confined within a rigid bony structure, the abdominal compartment can change shape during increasing IAV. During the initial phase of increasing IAV (e.g., laparoscopic insufflation), IAP only rises minimally (linear ‘reshaping phase’ from spherical to circular shape). This is followed by a ‘stretching phase’ of the rectus abdominis muscle (curvilinear phase) and finally, when further IAV is added, only small increases in IAV will result in dramatic increase in IAP (exponential ‘pressurization phase’) (Fig. 2) [6, 7]. During the stretching phase, the shape of the abdomen will change from elliptical to spherical. This change in shape is mainly due to an increase in the antero-posterior diameter and a decrease in the transverse diameter (transverse plane) of the internal abdominal perimeter [8–12].

Predictors for stretching and reshaping capacity

Factors determining the reshaping properties of the abdominal wall and diaphragm are not well understood but the mechanical properties are related to $C_{ab}$. The stretching capacity is influenced by body anthropomorphic (weight, height, body mass index [BMI]), age, sex and visceral versus subcutaneous fat distribution [11]. Comorbidities like chronic obstructive lung disease (COPD) with emphysema (flattening of diaphragm), fluid overload (tissue and interstitial edema) or burn injury (with circular eschars) all have negative effects on stretching capacity. Android obesity usually results in increased visceral fat and a sphere-like baseline shape of the abdominal cavity with poor stretching capacity, whereas gynoid obesity presents with more subcutaneous fat for the same BMI or abdominal perimeter (Fig. 3). In gynoid obesity, the internal abdominal perimeter is elliptical. Patients with an ellipse-shaped internal perimeter have a much greater stretching capacity (and thus very good $C_{ab}$).

Abdominal pressure-volume relationship

A linear abdominal PV relationship has been described previously. However, this was mainly in studies where the observed IAP values were < 15 mmHg. During laparoscopy with limitation of insufflation pressures at 12 to 15 mmHg, the IAV did not reach a critical point at which an exponential increase in IAP occurred [13]. As discussed above, the initial phase of the PV curve may indeed be linear (as observed during laparoscopy) but the remaining part is curvilinear or rather exponential [13–15]. Because of this exponential relationship, it is important to know both the shape and the position on the curve, as the actual position will determine the corresponding $C_{ab}$. In patients with IAH a small increase in IAV may push them into ACS (especially if $C_{ab}$ is low) and, vice versa, in patients with ACS a small decrease in IAV (with paracentesis) may result in a dramatic improvement in IAP.

Measurement

Intra-abdominal pressure

Because of the fluid-like nature of the abdomen, following Pascal’s law, the IAP can be measured in nearly every part of it. Rectal, uterine, inferior vena cava, bladder and gastric pressure measurements have all been described [16]. The use of direct intraperitoneal pressure measurement cannot be advocated in patients because of the complication risks, such as bleeding or infection. Bladder pressure measurements have been forwarded as the gold standard with the technique suggested in the WSACS consensus guidelines [1].

Intra-abdominal volume

The abdominal volume is more difficult to measure. However, it can be estimated by anthropomorphic...
indices and imaging techniques. Anthropomorphic-based indices for estimation of IAV have been described in obesity [17]. However, BMI does not correlate with $C_{ab}$ but does correlate with IAP at the resting volume. This only applies in healthy individuals and sometimes in critically ill patients. The external abdominal perimeter (or circumference), although often used in the past, correlates reasonably with IAV, but poorly with IAP [18]. Changes in external abdominal perimeter over time on the other hand may correlate well with changes in IAP [18]. Another useful parameter is the waist-to-hip ratio. The waist is the smallest horizontal girth between the rib cage and iliac crest and the hip is the largest horizontal girth between waist and thigh. The waist-to-hip ratio correlates with IAP in men only [17]. A promising index is the abdominal volume index (AVI). A formula developed for calculating AVI estimates the overall abdominal volume between the symphysis pubis and the xiphoid process. This measure theoretically includes intra-abdominal fat and adipose volumes, with the waist and the hip dimensions. Although this index is superior to BMI, waist-to-hip ratio, and waist circumference, it has not yet been correlated to IAP [19]. Recently, techniques for estimating abdominal volume via three-dimensional (3D) ultrasound, water-suppressed breath hold magnetic resonance imaging (MRI), and computed tomography (CT) have been described. These techniques have not yet gained entrance to the intensive care unit (ICU). Although 3D ultrasound cannot measure IAV in toto, it estimates the volumes of separate intra-abdominal organs. MRI and CT techniques calculate the visceral and subcutaneous fat volume or thus the volume of the adipose tissue. Quantitative CT analysis assessing volume, density and weight of abdominal organs may be a promising tool for the future [9, 10, 20, 21].

**Abdominal compliance**

**Qualitative measurement of abdominal wall tension during palpation**

The grade of indentation at the site where the downward force is applied can be measured during palpation of the abdomen. Palpation examines intra-abdominal tension, passive and active muscle tension. However, it is not able to quantify $C_{ab}$ properly nor has it been validated in the clinical setting. The use of an abdominal tensiometer has also been described; however, this technique is only in its infancy [22].

**PV relationship during laparoscopy with CO$_2$ pneumoperitoneum**

It has been observed that the compliance of the abdominal cavity decreases when additional volume is added [23]. The linear abdominal PV curve changed to a rather exponential shape when a pressure of 15 mmHg was achieved by insufflation of CO$_2$ [13, 14]. In studies, the initial $C_{ab}$ at the beginning of the CO$_2$ inflation varied between 333 and 400 ml/mmHg and at higher IAV (with corresponding IAP > 15 mmHg), the $C_{ab}$ decreased to 60 and 90 ml/mmHg [3]. Similar relationships have been described with addition or removal of gastric contents [3].

**PV relationship during drainage or addition of abdominal free fluid**

Measurements of $C_{ab}$ have been performed in humans by IAP assessment with at least two corresponding IAV values by addition of abdominal fluid during peritoneal
dialysis or by drainage of intra-abdominal fluid (ascites in liver cirrhosis, peripancreatic fluid or pseudocyst, serous fluid collections in trauma or burns) [2–4].

**Interactions between different compartments**

**Polycompartment model**

Being linked and bound by the diaphragm, the thoracic and abdominal compartments cannot be treated in isolation. Applied airway pressure ($P_{aw}$) by mechanical ventilation is transmitted to the lungs, pleural ($P_{pl}$) and abdominal spaces (IAP). In a simplified model, the lung and thorax are in series and coupled to the diaphragm and abdomen in series. Changes in IAP are paralleled by changes in $P_{pl}$. Changes in thoracic compliance will be reflected by changes in abdominal compliance and vice versa; as a consequence, increased IAP will result in reduced chest wall compliance. The interactions between different compartments have been referred to as the polycompartment model and syndrome [24, 25]. For example, transmission of airway pressures to the abdomen results from interactions between the thoracic and abdominal compartment and the percentage of pressure transmission is called the thoraco-abdominal index (TAI) of transmission. This occurs in patients receiving positive pressure ventilation, application of positive end-expiratory pressure (PEEP), presence of intrinsic or auto-PEEP or a tension pneumothorax. Conversely, transmission of pressure from the abdomen to the thorax is called the abdomino-thoracic index (ATI) and occurs in any physiologic (pregnancy) or pathologic condition associated with increased IAP; the ATI ranges from 20 to 80 % and is on average 50 % [26, 27]. The effects of increased IAP on end-organ function are numerous: neurologic, respiratory, cardiovascular and renal adverse effects have all been described in patients with IAH and ACS. Increased IAP leads to diminished venous return, necessitating more fluid loading, causing mesenteric vein compression and venous hypertension, finally triggering a vicious cycle.

**Estimation of abdominal compliance during low flow pressure volume loop**

$C_{ab}$ can be estimated by analysis of the dynamic changes caused by mechanical ventilation on IAP. During a low flow PV loop to determine the best PEEP, one can observe the change in mean IAP. The compliance obtained by this maneuver can be calculated as follows:

$$C_{abPV} = \Delta V_T/\Delta \text{mean IAP}$$

with $\Delta V_T$ the insufflated tidal volume and $\Delta \text{IAP}$ the difference between mean IAP at the end and start of the PV loop.

**Estimation of abdominal compliance during mechanical ventilation**

Whilst looking at the effects of tidal volume excursions on IAP and by calculating the difference between IAP$e_i$ and IAP$e_e$, one can also obtain an idea of $C_{ab}$ [28]:

$$C_{abTV} = V_T/\Delta IAP$$

The higher the respiratory excursions seen in a continuous IAP tracing, the lower the $C_{ab}$ (for the same tidal volume). Alternatively, the higher the IAP, the higher the $\Delta IAP$ or the lower the $C_{ab}$.

**Calculation of abdominal pressure variation**

As discussed previously, the higher the APV for any given IAP, the lower the $C_{ab}$ and vice versa, the lower the $C_{ab}$, the higher the APV; hence APV can be used as a non-invasive and continuous estimation of $C_{ab}$.

**Respiratory abdominal variation test (RAVT)**

A final non-invasive method for estimation of $C_{ab}$ can be done by performing a respiratory abdominal variation test (RAVT) (Fig. 4). The $C_{ab}$ obtained with RAVT correlates with the $C_{ab}$ obtained from $\Delta IAP$ during
mechanical ventilation; increasing tidal volume increases IAP\textsubscript{ei} while increasing PEEP increases IAP\textsubscript{ee}.

\[ C_{abRVT} = \Delta VT / \Delta IAP_{ei} \]

**Prognostic and predictive factors related to abdominal compliance**

Theoretically, \( C_{ab} \) allows prediction of complications during laparoscopy and mechanical ventilation, identification of patients who would benefit from delayed abdominal closure, those in whom to monitor IAP, and those at risk during prone ventilation, etc. Therefore, prediction of poor or high \( C_{ab} \) can be clinically important.

**Conditions associated with decreased abdominal compliance**

Aside from risk factors for IAH, patients should also be screened for risk factors for decreased \( C_{ab} \). These are listed in Table 1 and can be divided into those related to body habitus and anthropomorphy; those related to comorbidities and/or increased non-compressible IAV; and those related to the abdominal wall and diaphragm [3].

Morbidly obese patients have a higher baseline IAP around 12–14 mmHg, and this is mainly related to the presence of central obesity [17, 29–32]. Morbidly obese patients with an android (mainly visceral and sphere shaped) fat distribution have a limited reserve to accommodate excess IAV than those patients who, for a similar BMI or abdominal perimeter, have a gynoid (mainly subcutaneous and ellipse shaped) fat distribution [17, 29]. On the other hand, subcutaneous fat accumulation may have a negative effect on the elastic properties of the abdominal wall, although the thin muscle layer may have a beneficial effect. Therefore, it is not possible to predict \( C_{ab} \) in obese patients; in general \( C_{ab} \) is decreased because of the increased baseline IAV.

**Conditions associated with increased abdominal compliance**

These are listed in Table 2 and can be divided into those related to body habitus and anthropomorphy; those related to absence of comorbidities and/or increased compressible IAV; and those related to abdominal wall and diaphragm. Chronic conditions will have higher \( C_{ab} \) for the same change in IAV as illustrated in Fig. 5.

Previous stretching of the abdominal fascia increases \( C_{ab} \). This can be explained by a gradual prestretching of the internal abdominal cavity perimeter during acute or progressive increased IAV (as is the case during laparoscopy, with pregnancy, peritoneal dialysis, cirrhotic ascites) [7–9, 33, 34], which leads to increased reshaping capacity. Prestretching or overdistension may indeed

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**Table 1 Factors associated with decreased abdominal compliance. Adapted from [2] with permission**

1) Related to anthropomorphy and demographics
   - Android composition (sphere, apple shape)
   - Increased visceral fat
   - Waist-to-hip ratio > 1
   - Short stature
   - Male sex
   - Young age (increased elastic recoil)
   - Obesity (weight, BMI)

2) Related to comorbidities and/or increased non-compressible intra-abdominal volume (IAV)
   - Fluid overload
   - Abdominal fluid collections, pseudocyst, abscess
   - Sepsis, burns, trauma and bleeding (coagulopathy)
   - Bowels filled with fluid
   - Stomach filled with fluid
   - Tense ascites
   - Hepatomegaly
   - Splenomegaly

3) Related to abdominal wall and diaphragm
   - Interstitial and anasarca edema (skin, abdominal wall)
   - Abdominal burn eschars (circular)
   - Thoracic burn eschars (circular)
   - Tight closure after abdominal surgery
   - Abdominal Velcro belt or adhesive drapes
   - Prone positioning
   - Head-of-bed > 45°
   - Umbilical hernia repair
   - Muscle contractions (pain)
   - Body builders (‘6-pack’)
   - Pneumoperitoneum
   - Pneumatic anti-shock garments
   - Abdominal wall bleeding
   - Rectus sheath hematoma
   - Correction of large hernias
   - Gastrochisis
   - Omphalocele
   - Mechanical ventilation (positive pressure)
   - Fighting with the ventilator
   - Use of accessory muscles
   - Use of positive end-expiratory pressure (PEEP)
   - Presence of auto-PEEP (tension pneumothorax)
   - Chronic obstructive pulmonary disease (COPD) emphysema
   - (diaphragm flattening)
   - Basal pleuropneumonia
result in tissue damage and fibrosis of the abdominal wall structure with lengthened muscle fibers and diminished elastic retraction capacity. History of a previous laparotomy may lead to scarring of the abdominal wall, which in combination with adhesions may cause decreased elasticity [33]. The Cab may be decreased or increased and the effect of previous laparotomy on baseline IAV and IAP is unpredictable. The use of external bandages (drapings, Velcro belt, etc.) or tight surgical closure causes a mechanical limitation; these should be avoided in high-risk patients and IAP should be measured during their use. In case of capillary leak, fluid overload and fluid collections, IAV and IAP will both increase while reshaping capacity and wall compliance will decrease.

**Treatment**

**How to decrease baseline IAP?**

In simple terms, in order to reduce IAP, either (additional) IAV has to be removed intra-luminally or intra-abdominally (e.g., weight loss, fluid removal via dialysis, ascites drainage, gastric suctioning, evacuation of abscess or hematoma, etc.), or the Cab has to be improved by increasing the internal abdominal cavity perimeter and surface area (pre-stretching, open abdomen treatment) [35, 36]. Weight loss and the resulting decrease in BMI will decrease IAP [37].

**How to reduce IAV?**

The evacuation of intra-luminal and intra-abdominal contents can be done, for example, via placement of a nasogastric tube with suctioning with or without gastroprokinetics (cisapride, metoclopramide or erythromycin). Paracentesis with evacuation of ascites and the placement of a rectal tube in conjunction with enemas and colonoprokinetics (prostigmin) may also reduce IAV [38]. Colonic pseudo-obstruction or Ogilvie’s syndrome may be treated with endoscopic decompression of large bowel or a surgical colostomy or ileostomy together with colonoprokinetics. When in doubt, imaging should be performed and ultrasound or CT guided drainage should be attempted in case of hematoma, abscess, fluid collections, etc. The correction of capillary leak and avoiding a

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**Table 2** Factors associated with increased abdominal compliance. Adapted from [2] with permission

| 1) Related to anthropomorphy and demographics |
|-----------------------------------------------|
| - Gynoid composition (ellipse, pear-shaped)   |
| - Waist-to-hip ratio < 0.8                    |
| - Peripheral obesity                          |
| - Preferentially subcutaneous fat             |
| - Height (tall stature)                       |
| - Old age (loss of elastic recoil)           |
| - Female sex                                 |
| - Lean and slim body                         |
| - Normal BMI                                 |
| 2) Related to absence of comorbidities and/or increased compressible intra-abdominal volume (IAV) |
| - Absence of deadly triad: normothermia, normal pH, normal coagulation |
| - Bowels filled with air                      |
| - Stomach filled with air                     |
| - Absence of fluid overload (second or third space fluid accumulation) |
| 3) Related to abdominal wall and diaphragm   |
| - Previous pregnancy                          |
| - Previous laparoscopy                        |
| - Previous abdominal surgery                  |
| - Abdominal wall lift                         |
| - Weight loss                                 |
| - Chronic intra-abdominal hypertension (IAH)  |
| - Umbilical hernia (before repair)            |
| - Burn escharotomy (thorax and/or abdomen)    |
| - Avoidance of tight closure                  |
| - Open abdomen with temporary abdominal closure|
| - Beach chair positioning                     |
| - Sedation and analgesia                      |
| - Muscle relaxation                           |
| - Bronchodilation                             |
| - Lung protective ventilation                 |
| - Pre-stretching of fascia (cirrhosis with ascites, peritoneal dialysis when fluid is drained from abdomen) |

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**Fig. 5 Abdominal compliance (Cab) in relation to baseline intra-abdominal pressure (IAP).** Bar graph showing mean values of Cab (ml/mmHg) per baseline IAP category (mmHg) in acute (light blue bars) and chronic (dark blue bars) conditions. Acute conditions are laparoscopy and evacuation of ascites, collections or hematomas in acutely ill patients, whereas chronic condition refers to peritoneal dialysis. Adapted from [3] with permission.
positive fluid balance will eventually lead to a decreased IAV by decreasing organ and bowel edema [39]. This can be achieved with (hypertonic) albumin in combination with diuretics (furosemide), correction of capillary leak (antibiotics, source control, ...), the use of colloids instead of crystalloids and eventually dialysis or continuous veno-venous hemofiltration (CVVH) with ultrafiltration [40]. Targeted APP with the use of vasopressors will reduce venocongestion and this will lower IAV (in analogy to the effect of norepinephrine on intracranial pressure and cerebral perfusion pressure) and dobutamine (but not dopamine) will improve splanchnic perfusion. Ascorbic acid has been associated with a reduced incidence of secondary ACS in burn patients, although its routine use has yet to be validated.

How to improve \( C_{ab} \)?

Improvement in \( C_{ab} \) should be performed in a stepwise approach as suggested by the WSACS consensus recommendations [1, 3].

**First step: ensure adequate sedation and analgesia**

Fentanyl should not be used as it may increase abdominal muscle tone while dexmedetomidine has superior effects over propofol. Thoracic epidural anesthesia has been shown to reduce IAP via an increase in \( C_{ab} \) [41].

**Second step: remove constrictive bandages and eschars**

Any tight abdominal closure, like a Velcro belt to prevent incisional hernia in a patient with abdominal hypertension and end-organ dysfunction, should be removed immediately. Likewise, escharotomies (abdominal but also thoracic) will increase \( C_{ab} \) while sternotomy will increase not only thoracic wall compliance but also \( C_{ab} \) [42–44]. Placing a chest tube in case of a tension pneumothorax or pleural effusion will also increase \( C_{ab} \).

**Third step: avoid prone and head of bed > 30° and consider reverse Trendelenburg position**

Body positioning, such as the Trendelenburg position, may lower bladder pressure; however, it may also compromise respiratory function [29]. The use of head-of-bed elevation > 30° may on the other hand increase bladder pressure and the head-of-bed 45° position will increase IAP by 5 to 15 mmHg [29]. Therefore, in patients with respiratory insufficiency who are mechanically ventilated, the anti-Trendelenburg position may be best to allow lung recruitment, oxygenation and ventilation [16]. During prone positioning there is merit in unloading the abdomen (abdominal suspension) as this will result in a decrease in chest wall compliance, while the effect of gravity will improve \( C_{ab} \) and decrease IAP. During laparoscopy, body position can also help to optimize the laparoscopic workspace IAV. The Trendelenburg position with head-of-bed at 20° provides the optimal workspace in lower abdominal laparoscopic surgery, while during upper abdominal laparoscopic surgery in obese patients, the beach-chair position (flexing the legs in reverse Trendelenburg) is optimal [45]. Laparoscopic insufflation pressures should at all times be limited to 15 mmHg. Higher working pressures cannot be routinely recommended in obese patients with high baseline IAP and in morbidly obese patients, open surgery seems the best option because of the high complication risk associated with pneumoperitoneum [31].

**Fourth step: lose weight and avoid fluid overload**

Similar to weight loss, avoiding a positive cumulative fluid balance and obtaining a negative fluid balance with the use of diuretics in combination or not with hypertonic solutions (albumin 20 %) [40, 46] will decrease interstitial edema of the abdominal wall and increase \( C_{ab} \). Fluid resuscitation should be guided by volumetric (and not barometric) preload indicators and, if central venous pressure (CVP) is used, transmural pressures should be calculated:

\[
CVP_{tm} = CVP_{ee} - IAP/2.
\]

In case diuretics do not have a sufficient effect, renal replacement therapy with hemodialysis or CVVH can be used [1, 3].

**Fifth step: use neuromuscular blockers**

Theoretically, the use of neuromuscular blockade should not only lower baseline IAP but also improve \( C_{ab} \) [1, 3]. However, some studies showed no additional increase in \( C_{ab} \) after full block of abdominal muscle contractions (guided by train of four) [7].

**Sixth step: less invasive surgery**

Recently a less invasive percutaneous endoscopic abdominal wall component separation (EACS) technique has been described [47]. With this technique, the abdominal capacity (maximal stretched volume) increased by 11 while IAP decreased from 15.9 ± 2.1 to 11 ± 1.5 mmHg (\( p < 0.001 \)) [47]. Another alternative for midline laparotomy is subcutaneous linea alba fasciotomy (SLAF), which seems a promising approach especially in secondary IAH and ACS [48].

When all the above listed treatment options fail to provide a sufficient decrease in IAP and IAV, the only definite solution is to perform a decompressive laparotomy that will assist with IAP, IAV and \( C_{ab} \) [49].
Conclusion

$C_{ab}$ is a measure of the ease of abdominal expansion, determined by the elasticity of the abdominal wall and diaphragm. It is expressed as the change in IAV per change in IAP (ml/mmHg). The $C_{ab}$ baseline in ‘resting condition’ is determined by the baseline IAP and IAV, the external and internal abdominal cavity perimeter and surface area and shape, the additional and maximal stretched volume, the presence of predisposing conditions and comorbidities as well as tissue properties of the fascia, abdominal wall and diaphragm. As such, $C_{ab}$ should be viewed separately from the abdominal wall and diaphragm compliance with its own specific elastic properties. $C_{ab}$ can be estimated based on demographic and anthropomorphic data and can be assessed by PV relationship analysis of the observed changes in IAP (mirroring induced changes in IAV). The abdominal PV relationship is believed to be linear up to pressures of 12–15 mmHg and increases exponentially thereafter. $C_{ab}$ can also be estimated non-invasively by examining the interactions between pressure variations in the thorax and abdominal compartment during positive pressure ventilation. $C_{ab}$ is one of the most neglected parameters in critically ill patients, although it plays a key role in understanding organ-organ interactions and the deleterious effects of unadapted IAV on IAP and end-organ perfusion. A large overlap exists between the treatment of patients with IAH and those with low $C_{ab}$, but when we identify the latter, we should potentially be able to anticipate and select the most appropriate medical or surgical treatment to avoid complications related to IAH or ACS.

Competing interests

Dr Manu Malbrain is member of the Executive Committee of the World Society of the Abdominal Compartment (WSACS) and current Treasurer; he is member of the medical advisory board of Pulsion Medical Systems (Maquet Getinge group). The other authors have no possible conflicts of interest related to the content of this paper.

Authors’ contributions

All authors read and approved the final manuscript.

Declarations

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