The morphology of the femoral footprint of the anterior cruciate ligament changes with aging from a large semicircular shape to a small flat ribbon-like shape

Rodolfo Morales-Avalos1,2,3 • Simone Perelli1,2 • Félix Vilchez-Cavazos3 • Tadeo Castillo-Escobedo3 • Víctor M. Peña-Martínez3 • Rodrigo Elizondo-Omaña4 • Santos Guzmán-López4 • José Ramón Padilla-Medina3 • Juan Carlos Monllau1,2

Received: 9 October 2021 / Accepted: 4 March 2022 / Published online: 22 March 2022
© The Author(s) 2022

Abstract
Purpose Compare the differences in the morphology of the ACL femoral footprint between the cadavers of the young and elderly in consideration of the degenerative physiological process that occurs with aging.
Methods The femoral footprint of the ACL was dissected in 81 knees of known gender and age (45 male/36 female). They were divided into four groups by age and gender, establishing 50 years as the cut-off point to divide patients by age. Three observers analyzed the femoral footprint dissections, and the shapes were described and classified. The area and morphometric characteristics of the femoral insertion of the ACL were determined and these were compared between genders and age groups.
Results The femoral footprint of the ACL from the cadavers of males younger than 50 years of age presented a semicircular morphology in 90% of the cases. In males aged more than 50 years, a ribbon-like morphology was found in 96% of the cases. In women less than 50 years old, the semicircular morphology was observed in 93.7% of the cases. In women aged over 50 years old, the ribbon-like morphology was found in 95% of the cases. A significant difference was observed between the prevalence rates of the morphologies, area size and measurements of the younger and older groups ($p<0.001$ for both genders).
Conclusions The femoral insertion of the ACL presents variations in its morphology, area size and morphometric characteristics over time. It goes from a large semicircular shape that almost contacts the posterior articular cartilage to a smaller, flattened ribbon-like shape that moves away from the edge of the articular cartilage. It is bounded anteriorly by the lateral intercondylar ridge. These findings should be considered to avoid employing reconstruction techniques in which femoral tunnels with oval or rectangular shapes are used in patients under 50 years of age because they do not correspond to the morphology of the femoral insertion of the ACL in this age group.

Keywords Anterior cruciate ligament • Aging • Area • Attachment • Femoral • Footprint • Insertion site • Morphology • Shape • Variations

Rodolfo Morales-Avalos
rodolfot59@hotmail.com

1 Knee and Arthroscopy Unit (ICATKNEE-EQUILAE), Department of Orthopedic Surgery, Institut Català de Traumatologia i Medicina de l’Esport (I.C.A.T.M.E.), Hospital Universitari Dexeus, Universitat Autònoma de Barcelona (U.A.B.), Barcelona, Catalunya, Spain
2 Department of Surgery and Morphologic Science, Orthopaedic Surgery Service, Hospital del Mar, Universitat Autònoma de Barcelona, Barcelona, Spain
3 Knee Unit, Department of Orthopedic Surgery and Traumatology, School of Medicine and University Hospital “Dr. José Eleuterio González”, Universidad Autonoma de Nuevo León (U.A.N.L), Monterrey, Nuevo León, México
4 Department of Human Anatomy, School of Medicine, Universidad Autonoma de Nuevo León (U.A.N.L.), Monterrey, Nuevo León, México
Anatomic anterior cruciate ligament (ACL) reconstruction attempts to recreate the native dimensions of the ACL, collagen orientation and insertion sites to recreate the function of the native ligament [32, 42]. It has already been shown that anatomic ACL reconstruction, in which the graft is placed within the native ACL insertions, might result in better knee stability when compared to nonanatomic techniques [6, 24]. Furthermore, the correct placement of the femoral tunnel is known as one of the most important factors influencing knee kinematics and clinical results in anatomic ACL reconstruction [23, 34].

ACL reconstruction was conventionally performed with a single-round femoral tunnel. However, some anatomical studies have revealed that the ACL femoral footprint is relatively elliptical in shape, not round [19]. Therefore, the use of bi-fascicular techniques or the realization of rectangular or oval tunnels have been proposed to try to imitate the native anatomy of the femoral insertion of the ACL in a more precise way. Still, some studies have described morphologies of the femoral insertion as being crescent-shaped, circular/round [12], semi-circular [10] or ovalized [10, 11]. Moreover, differences in the size of the femoral insertion have been described. A few studies have reported a long femoral insertion that extends backward to the articular cartilage margin [3, 7, 12, 18, 29], whereas other studies have described a relatively narrow insertion area [11, 26, 40].

Due to this confusion, a large number of anatomical studies have been carried out that have tried to precisely define the morphological characteristics of the femoral insertion of the ACL [7, 10–12, 16, 19, 34, 39, 40]. However, most of those studies were carried out with small samples and with elderly cadavers, which could lead to errors in the determination of the true morphological characteristics of the ACL. In addition, on other occasions, they do not make a clear distinction between the analysis of the direct insertion (mid-substance insertion) and the indirect insertion (fan-like extension) of the ACL.

A recent study determined that the tibial insertion of the ACL presents significant morphological variations with age [27]. Therefore, it is thought that similar changes may occur at the femoral insertion. The aim of the study was to compare the differences in the morphology of the ACL femoral footprint between the cadavers of the young and elderly due to a degenerative physiological process that occurs over time. The hypothesis is that there are significant variations in the shape of the femoral insertion of the ACL between the cadavers of younger people and older people. The results of this study will help to determine the normal shape and position that the femoral tunnel should have in a more individualized way.

This study was approved by the Institutional Review Board and Ethics Committee of the School of Medicine and University Hospital “Dr. Jose Eleuterio Gonzalez” of the Universidad Autonoma de Nuevo Leon with registration number OR16-00007. The study was carried out in accordance with the World Medical Association Declaration of Helsinki of 1964 and its revision in 2013 [45]. An anatomical, descriptive, observational and comparative study was performed with 88 non-paired, formalin-fixed human cadaver knees from the Mexican population is included.

The cadavers were collected from three distinct departments of human anatomy between 2016 and 2020. All specimens were over 18 years of age at the time of death. The gender, weight, and height of each cadaver were documented. The cause of death and the most important clinical information for each corpse was known and varied between the cadavers of the young and elderly. Head trauma was predominant in the young group and myocardial infarction and metabolic disorders in the elderly group. Unequivocally so, none of the causes of death or medical history of the included cadavers influenced the execution and results of this study.

The sample size was determined based on the availability of cadavers of individuals under 50 years of age. Data from a previous study of ACL morphology confirmed that the sample size was sufficient to detect differences among ages [27]. Furthermore, a post-hoc power analysis was performed to assess the adequacy of the sample size. Additionally, the goal of the study was for it to be done with the largest sample reported in the literature. The sample was divided into four groups according to age and gender: males and females younger and older than 50 years. This cut-off age was used based on a previous study that showed statistically significant differences in the tibial footprint morphology of the ACL [27].

All the knees were analyzed in phases to make sure they fulfilled the inclusion criteria. Before being included in the study, every specimen underwent an anteroposterior radiograph to exclude knees that presented an intraarticular fracture sequela, the presence of orthopedic implants or congenital bone anomalies. However, they were not used for the radiographic classification of osteoarthritis. In the inspection, those that presented scars from previous surgical interventions were excluded. Those knees that, at the time of the dissection, presented an ACL or macroscopic rupture of the posterior cruciate ligament (PCL), advanced osteoarthritis (Outerbridge Grade IV) or macroscopic degenerative changes in the synovial membrane that impaired adequate observation or dissection of structures of interest were excluded. Furthermore, the presence of osteophytes in the
medial region of the lateral femoral condyle, which could interfere with the measurements of distances between the ACL attachment and the articular cartilage of the condyle, was considered criteria for exclusion. A knee surgeon (SP) and an anatomist (SGL) independently reviewed the specimens for inclusion.

**Dissection technique**

Prior to dissection, the specimens were submitted to a 10% formaldehyde fixative solution and stored in a mixture of 54% ethylene glycol, 40% ethanol and 6% formaldehyde with colorant (CTR Scientific®, Monterrey, Mexico). Subsequently, the specimens were kept for 60 days in liquid glycerin [2].

The dissection technique was standardized and performed in the same way by all the team members to ensure consistency, and was based on our own experience and the dissection protocols reported in previous studies [3, 16, 19, 26, 34, 37, 39, 40]. The team consisted of a knee surgeon (FVC), an anatomist (REEO), and a senior orthopedic surgery and traumatology resident (JRPM).

The limbs were amputated at two sites, the first at the level of the thigh at 30 cm from the knee joint line and the other at the leg at 20 cm from the knee joint line. During the dissections, the knees were placed in a mechanical press that kept the knees in full extension and made flexion at 30°, 60° and 90° possible without any translational or rotational forces.

All superficial soft tissues on the anterior, posterior, medial and lateral surfaces of the knee were removed up to the joint capsular plane. The entire extensor apparatus was resected distally from the anterior tibial tuberosity and subsequently removed. After exposing the anterior side of the knee joint, the synovial tissue and the Hoffa fat pad were carefully dissected and separated from the joint soft tissue structures (meniscus and transverse ligament). The entire joint capsule, tibial and fibular collateral ligaments, menisco-femoral ligaments, posterior cruciate ligament and synovial tissues were carefully excised.

Starting from the uppermost point of the intercondylar notch, the femur was separated along the sagittal plane with an oscillating saw (Precision 7, Stryker®, Madrid, Spain). This was done to observe the full medial wall of the lateral femoral condyle and the lateral intercondylar ridge (resident’s ridge). Care was taken to avoid injury to the ACL or its bony insertion. Exposure after the medial condylectomy made for an excellent view of the femoral attachment of the ACL. The anteromedial and posterolateral fascicles (AM and PL) were identified by observing the orientation of the fibers and the differences in the tension pattern in the range-of-motion. The AM bundle fibers become taut during flexion, while PL bundle fibers become taut by extension. It is important to mention that it was not possible to show a division into fascicles in all cases. Thus, it was only done on specimens where it was possible. It is worth noting that it was particularly difficult in the elderly specimens. The synovial envelope of the ACL bundles was carefully excised with a surgical blade and then sutures with different colors were passed around each bundle to identify them when it was possible. A meticulous dissection of the ACL fibers was performed up to their osseous insertion in the lateral femoral condyle. The insertional fibers were carefully separated from the surrounding synovial tissue while registering the presence of the indirect ACL insertion fibers or “fan like” extension fibers by identifying a macroscopically visible fold between the direct and indirect insertion of the ACL [39].

At the same time, the relationship of the femoral insertion to the lateral intercondylar ridge was analyzed using a microsurgical microscope with 10× magnification (Carl Zeiss OPMI® Pico, Berlin, Germany). To properly identify the footprint without damaging it during dissection, an ink stain was applied on the bone immediately around the periphery of the entire femoral insertion site (direct + indirect portion) by one of the authors who did not participate in the dissections or in the morphological classification of the femoral footprint (VMPM) [16]. Then, the ACL was delicately excised as closely as possible to the intercondylar wall of the lateral condyle in 90° of flexion using a No. 11 scalpel blade. After that step, the previous ink mark was removed. The remnant of the femoral insertion...
after its transection as well as the previous division of its fascicles served for its later classification.

Following a method previously described, all the different ACL footprint portions were marked with ink: (1) the whole femoral ACL footprint, (2) the direct insertion, (3) the indirect insertion (fan-like extension), (4) the whole AM and PL area, (5) the direct insertion area of AM and PL bundles and (6) the fan-like extension fibers area of AM and PL bundles (Fig. 1) [16]. The points 4–5–6 were marked only when the AM and PL bundles were clearly identifiable.

Subsequently, the team of surgeons proceeded to measure the following morphometric parameters using a millimeter digital caliper with a precision of 0.01 mm (Mitsutoyo Digimatic w/Absolute Encoders-Series 500, Tokyo, Japan). Figure 2 details each of the landmarks used. The landmarks were defined by consensus in the dissection team when it was done.

1. Proximodistal diameter of the direct ACL attachment area (long axis) (A–B)
2. Anteroposterior diameter of the direct ACL attachment area (short axis) (C–D)
3. Horizontal distance between the proximal border of the direct ACL attachment and the adjacent margin of the articular cartilage (A–E)
4. Horizontal distance between the distal border of the direct ACL attachment and the adjacent margin of the articular cartilage (B–G)
5. Horizontal distance between the posterior extent of the direct ACL attachment and the posterior articular surface (D–G)
6. Horizontal distance between the anterior extent portion of the direct ACL attachment and the anterior articular surface (C–H)
7. Vertical distance between the distal border of the direct ACL attachment and the inferior articular surface (B–I).

Afterwards, the ink was again completely removed, and a reference marker was used as the specimens were photographed using an 18.7-megapixel high-resolution digital camera (model EOS 1300D, Nikon Corp., Tokyo, Japan) positioned on a professional tripod (Canon Inc., Tokyo, Japan). The photograph consisted of an accurate view of the medial wall of the lateral femoral condyle perpendicular to the femoral insertion with the knees placed at 0° and 90°
of knee flexion. The camera lens was placed 25 cm parallel to the articular surface, and the ACL femoral footprint was at the center of the image. In this way, a high-resolution image of each sample was recorded in case of deterioration and to be used to resolve differences between observers in the post-consensus meeting. The same images were used to calculate the area of the ACL femoral footprint and to repeat the same morphometric analyses carried out manually.

All dissections and photographs were evaluated by three independent observers. There were three knee surgeons (RMA, TACE and JCM) blind to the age and gender of the specimens. It was carried out just after the dissection and in a second revision after 2 weeks. The specimens were again evaluated in a different order from the first evaluation. Moreover, the 2nd round of evaluations was blinded to the results of the first evaluation. During the interval, the specimens were stored in a cold room for preservation. After the evaluations were concluded, the differences were reviewed in a consensus meeting using a nominal group technique without a hierarchy. The shape of the femoral footprint was described as ribbon-like (or flattened), oval/elliptical, round/circular, semicircular, small-semicircular or undetermined in accordance with the classifications previously proposed [3, 18, 19, 26, 34, 35, 37].

The images were downloaded to a personal computer. The Image J software version 1.49 (National Institute of Health, Bethesda, USA, http://rsbweb.nih.gov/ij/) was used to perform the previously described measurements and compare them with those made at the time of dissection. Moreover, the software was used to estimate the footprint area after adjusting the computer images to the actual knee size. The whole ACL area and the whole direct and indirect insertion area were always calculated. In cases where a precise definition of the two bundles was possible, the whole area and the direct insertion area as well as the fan-like extension fibers area of the AM and PL bundles were also calculated [16]. The accuracy of the area measurement was less than 0.1 mm and 0.1 mm².

### Statistical analysis

Statistical analyses were performed using SPSS software package (version 19.0 for Windows XP). Intra and inter-rate reliability was calculated using the Cohen’s kappa and Fleiss Kappa coefficients, respectively. The Mann–Whitney U test was used to determine the significance of the differences between the ages of the different groups. The Chi-square test was used to compare genders within the same age group and to compare age groups between specimens of the same gender. Because we performed multiple comparisons, we used the Bonferroni correction method to calculate the appropriate alpha value for which associations can be considered statistically significant. The following formula was used to calculate the Bonferroni-corrected alpha: pre-specified alpha/number of comparisons. A p value of less than 0.05 was considered significant and all tests were two-tailed. An a priori sample size estimation was not done as the decision was taken to use all the samples that were available in our laboratory, regardless of the result. Post-hoc power analyses were performed based on the main outcome of finding differences between different age groups. The asymptotic relative efficiency method was performed for the Mann–Whitney U tests. The results are presented as median observed power and median sample required for achieving 80% power on an alpha level of 0.05 based on observed differences.

### Results

In the final analysis, 81 knees were included (45 male and 36 female). The distribution of the sample by gender and age is shown in Table 1. From the original sample of 88 knees 7 were eliminated. Advanced osteoarthritis of the tibio-femoral or patello-femoral joint was present in 3 of them, 2 had scars that were probably the result of previous knee surgery, and 2 had a complete ACL tear. The mean age of the specimens was 87 years ± 8.3 for the group of males over 50 yearsold, 28 years ± 6.2 for the group of males under 50 years of age, 82 years ± 9.2 for the females over 50 years old and 26 years ± 7.4 for the females under 50. Significant differences in the ages of the specimens from different genders were not observed. The mean weight and height of the cadaveric specimens were 79.5 kg ± 13.6 and 1.66 ± 0.08, respectively. The results of interobserver analysis were concordant (Kappa = 0.93) and the results of the intraobserver analysis were always the same (Kappa = 1). No difference was detected between the morphometric values obtained from the cadavers and from the images.

### ACL femoral footprint shape

The knees from the cadavers of males younger than 50 years of age presented a “semicircular” morphology in 90% (n = 18/20) of the cases (Fig. 3A, B). In the group of males over 50 years old, a ribbon-like appearance was founded in 96% (n = 24/25) of the cases (Fig. 3C, D). In the group of

**Table 1 Distribution of the sample by gender and age of the knees included in the study**

| Category          | Semicircular | Ribbon-like |
|-------------------|--------------|-------------|
| Male > 50 (n = 25)| 1 (4%)       | 24 (96%)    |
| Male < 50 (n = 20)| 18 (90%)     | 2 (10%)     |
| Female > 50 (n = 20)| 1 (5%)   | 19 (95%)    |
| Female < 50 (n = 16)| 15 (93.75%)| 1 (6.25%)   |
women less than 50 years old, the semicircular morphology was observed in 93.7% ($n=15/16$) of the cases. In women over 50 years, the ribbon-like morphology was found in 95% ($n=19/20$) of the cases (Table 1). No other types of morphologies previously described in the literature were found.

The chi-square test was applied to compare the results of the prevalence rates of the different observed morphologies. When independently comparing the group of men < 50 years vs males > 50 years, females < 50 years vs females > 50 years and the totality of the knees < 50 years all the knees vs > 50 years (regardless of gender), the value of $p$ was < 0.001. However, no differences were observed between males and females of the same age group (Table 2).

### Macroscopic anatomy

In young cadavers of both genders, the most prevalent morphology was semicircular, which had a straight anterior border that contacts the lateral intercondylar ridge and its posterior side convex that almost contacts the posterior articular cartilage. The indirect fibers in this group were scarce and they occupied a small area in the portion closest to the posterior articular cartilage. It was possible to identify the two ACL bundles separately in 100% of the cases. In all knees, the direct insertion site and the fanlike extensions were successfully divided. In the cadavers of people of advanced age, the direct femoral insertion moves away from the posterior edge of the articular cartilage and is kept in bounded anteriorly by the lateral intercondylar ridge, having a continuity with the posterior cortex of the femur. The insertion morphology is thinner and has the shape of a flattened ellipse, simulating a ribbon. It is smaller compared to its younger counterpart and the indirect insertion fibers are more abundant while occupying a larger area and almost come into contact with the posterior edge of the articular cartilage. In some cases (8/45), it was not possible to identify the two bundles of the ligament, individually.

### Morphometries and areas

The average measurements of the morphometries and areas of the study groups are shown in Tables 3 and 4. Relative to gender, there were no significant differences for substantially few variables. One exception was the entire area of the ACL (127 mm$^2 \pm 23$ in Women vs. $145 \text{ mm}^2 \pm 21$ in men, $p=0.01$ and $111 \text{ mm}^2 \pm 18$ vs $123 \text{ mm}^2 \pm 19$, $p=0.03$ for < 50 and > 50 years old, respectively). However, a pattern of greater morphometries and areas of the ACL in men than in women was observed. Moreover, the distance from the posterior edge of the insertion to the articular cartilage was always greater in women. Nonetheless, all these results were not significant (Table 3).

Most of the distances between the articular cartilage and the direct femoral insertion of the ACL (the distances up to the posterior articular cartilage) were significantly greater in the older group. At the same time, it was noted that the anteroposterior diameter of the direct insertion of the ACL significantly decreased in both genders with the passage of time. The ACL as well as all the areas (direct and indirect) of the AM and PL fascicles do not present significant variations with respect to age. However, the proportion between

---

**Table 2** Values of $p$ obtained by comparing the different study groups relative to age and gender

| Comparison                        | $p$ value |
|-----------------------------------|-----------|
| males < 50 years vs. males > 50 years | < 0.001   |
| females < 50 years vs. females > 50 years | < 0.001   |
| total knees < 50 years vs. total knees > 50 years | < 0.001   |
| males > 50 years vs. females < 50 years | n.s.      |
| males > 50 years vs. females > 50 years | n.s.      |
| Total male knees vs. total female knees | n.s.      |
the direct and indirect areas between the younger and older knees does show significant variations over time. The whole area of the ACL does not show significant variations but the proportion between their direct and indirect insertion areas changed with aging, the direct areas being significantly higher in the under 50 groups and the indirect insertion areas significantly greater in the over 50 groups (Table 4).

### Discussion

The main finding of the present study was that the femoral insertion of the ACL presents variations in its morphology over time. It goes from being large and semicircular in shape in young subjects to a smaller and flattened ribbon-like shape in older subjects, which confirms the initial hypothesis. In the same way, significant differences were detected in most of the morphometric parameters and areas analyzed between the different age groups of the same gender. Additionally, there were no differences between genders in the same age group.

---

**Table 3** Comparison between the average values obtained in each gender for the same age group

| Category                                                                 | Age range (years) | Female (mean ± SD) | Male (mean ± SD) | Female vs. male (p value) |
|--------------------------------------------------------------------------|-------------------|--------------------|------------------|--------------------------|
| Proximodistal diameter of the direct ACL attachment area (Long axis)     | <50               | 16.55 mm ± 2.42    | 17.02 mm ± 2.24  | n.s.                     |
|                                                                          | >50               | 13.22 mm ± 1.85    | 15.44 mm ± 1.95  | n.s.                     |
| Anteroposterior diameter of the direct ACL attachment area (Short axis)  | <50               | 9.32 mm ± 1.13     | 11.22 mm ± 1.4   | n.s.                     |
|                                                                          | >50               | 3.12 mm ± 0.72     | 4.92 mm ± 0.85   | n.s.                     |
| Horizontal distance between the proximal border of the direct ACL attachment and the adjacent margin of the articular cartilage | <50               | 2.2 mm ± 0.55      | 2.0 mm ± 0.48    | n.s.                     |
|                                                                          | >50               | 7.3 mm ± 2.4       | 6.7 mm ± 1.93    | n.s.                     |
| Horizontal distance between the distal border of the direct ACL attachment and the adjacent margin of the articular cartilage | <50               | 2.5 mm ± 0.42      | 2.3 mm ± 0.66    | n.s.                     |
|                                                                          | >50               | 8.8 mm ± 1.76      | 8.5 mm ± 2.12    | n.s.                     |
| Horizontal distance between the posterior extent of the direct ACL attachment and the posterior articular surface | <50               | 2.3 mm ± 0.61      | 2.1 mm ± 0.59    | n.s.                     |
|                                                                          | >50               | 8.2 mm ± 2.02      | 7.9 mm ± 1.75    | n.s.                     |
| Horizontal distance between the anterior extent portion of the direct ACL attachment and the anterior articular surface | <50               | 13.21 mm ± 1.25    | 14.32 mm ± 1.66  | n.s.                     |
|                                                                          | >50               | 14.55 mm ± 1.87    | 15.02 mm ± 2.04  | n.s.                     |
| Vertical distance between the distal border of the direct ACL attachment and the inferior articular surface | <50               | 2.02 mm ± 0.88     | 1.55 mm ± 0.72   | n.s.                     |
|                                                                          | >50               | 2.97 mm ± 1.22     | 2.43 mm ± 1.07   | n.s.                     |
| Whole femoral footprint area                                              | <50               | 127 mm² ± 23       | 145 mm² ± 21     | 0.012*                   |
|                                                                          | >50               | 111 mm² ± 18       | 123 mm² ± 19     | 0.03                     |
| Whole direct insertion area                                               | <50               | 104 mm² ± 17       | 122 mm² ± 20     | n.s.                     |
|                                                                          | >50               | 57 mm² ± 11        | 61 mm² ± 15      | n.s.                     |
| Whole indirect insertion area                                             | <50               | 19 mm² ± 6        | 17 mm² ± 4       | n.s.                     |
|                                                                          | >50               | 47 mm² ± 14       | 56 mm² ± 15      | n.s.                     |
| Whole AM footprint area                                                   | <50               | 67 mm² ± 15       | 78 mm² ± 13      | n.s.                     |
|                                                                          | >50               | 55 mm² ± 13       | 62 mm² ± 14      | n.s.                     |
| Direct insertion area of AM bundle                                        | <50               | 52 mm² ± 10       | 63 mm² ± 11      | n.s.                     |
|                                                                          | >50               | 26 mm² ± 7        | 32 mm² ± 8       | n.s.                     |
| Indirect insertion area of AM bundle                                      | <50               | 10 mm² ± 3        | 12 mm² ± 3       | n.s.                     |
|                                                                          | >50               | 25 mm² ± 5        | 34 mm² ± 8       | n.s.                     |
| Whole PL footprint area                                                   | <50               | 59 mm² ± 10       | 65 mm² ± 11      | n.s.                     |
|                                                                          | >50               | 53 mm² ± 8        | 58 mm² ± 9       | n.s.                     |
| Direct insertion area of PL bundle                                        | <50               | 48 mm² ± 5        | 51 mm² ± 6       | n.s.                     |
|                                                                          | >50               | 24 mm² ± 3        | 29 mm² ± 5       | n.s.                     |
| Indirect insertion area of PL bundle                                      | <50               | 10 mm² ± 1        | 12 mm² ± 2       | n.s.                     |
|                                                                          | >50               | 22 mm² ± 5        | 28 mm² ± 7       | n.s.                     |

We used the Bonferroni correction method to determine the p value at which the comparisons would be considered statistically significant due to multiple comparisons. The Bonferroni-corrected alpha value in these comparisons is 0.0125 instead of the traditional 0.05. Significant p values at this threshold are marked with an asterisk.
One type of tissue at the femoral attachment was described as dense mid substance fibers that are attached to a narrow oval area on the lateral condyle (direct insertion). Another was a thin, membranous, peripheral attachment of fibers that spread out towards the posterolateral condyle, which increases the area of the insertion site (a fan-like extension or indirect insertion site) [33]. The shape of the femoral footprint was described as ribbon-like (or flattened) [37], oval/elliptical, [3, 18, 19, 21, 26, 34, 35, 38] round/circular [10, 12], or semicircular [7]. In this study, a significant difference between the morphology was seen between cadavers of those younger and older than 50 years. In the older than 50, a thin structure with its greater diameter from proximal to distal in the shape of a ribbon-like was observed, similar to the one described by Smigielski [37] in a study with cadavers with a mean age of 67 years. In people younger than 50, a large semicircular structure, similar to the one described by Ferretti [7], was found. The latter study was conducted on specimens with a mean age of 75, and the shape differs from the one in the present study.

We used the Bonferroni correction method to determine the p value at which the comparisons would be considered statistically significant due to multiple comparisons. The Bonferroni-corrected alpha value in these comparisons is 0.0125 instead of the traditional 0.05. Significant p values at this threshold are marked with an asterisk.

### Table 4
Comparison between the average values obtained in each age group for the same gender

| Category                                                                 | Gender | < 50 years (mean ± SD) | > 50 years (mean ± SD) | < 50 years vs > 50 years (p value) |
|--------------------------------------------------------------------------|--------|------------------------|------------------------|-----------------------------------|
| Proximodistal diameter of the direct ACL attachment area                  | Female | 16.55 mm ± 2.4         | 13.22 mm ± 1.8         | n.s.                              |
|                                                                           | Male   | 17.0 mm ± 2.2          | 15.44 mm ± 1.9         | n.s.                              |
| Anteroposterior diameter of the direct ACL attachment area                | Female | 9.32 mm ± 1.1          | 3.12 mm ± 0.72         | <0.0001*                          |
|                                                                           | Male   | 11.22 mm ± 1.4         | 4.92 mm ± 0.85         | <0.0001*                          |
| Horizontal distance between the proximal border of the direct ACL        | Female | 2.2 mm ± 0.55          | 7.3 mm ± 2.4           | <0.0001*                          |
| attachment and the adjacent margin of the articular cartilage            | Male   | 2.0 mm ± 0.48          | 6.7 mm ± 1.93          | <0.0001*                          |
| Horizontal distance between the distal border of the direct ACL          | Female | 2.5 mm ± 0.42          | 8.8 mm ± 1.76          | <0.0001*                          |
| attachment and the adjacent margin of the articular cartilage            | Male   | 2.3 mm ± 0.66          | 8.5 mm ± 2.12          | <0.0001*                          |
| Horizontal distance between the posterior extent of the direct ACL       | Female | 2.3 mm ± 0.61          | 8.2 mm ± 2.02          | <0.0001*                          |
| attachment and the posterior articular surface                           | Male   | 2.1 mm ± 0.59          | 7.9 mm ± 1.75          | <0.0001*                          |
| Horizontal distance between the anterior extent portion of the direct   | Female | 13.21 mm ± 1.25        | 14.55 mm ± 1.87        | n.s.                              |
| ACL attachment and the anterior articular surface                        | Male   | 14.32 mm ± 1.66        | 15.02 mm ± 2.04        | n.s.                              |
| Vertical distance between the distal border of the direct ACL            | Female | 2.02 mm ± 0.88         | 2.97 mm ± 1.22         | n.s.                              |
| attachment and the inferior articular surface                           | Male   | 1.55 mm ± 0.72         | 2.43 mm ± 1.07         | n.s.                              |
| Whole femoral footprint area                                             | Female | 127 mm² ± 23           | 111 mm² ± 18           | 0.02                              |
|                                                                           | Male   | 145 mm² ± 21           | 123 mm² ± 19           | 0.0006*                           |
| Whole direct insertion area                                              | Female | 104 mm² ± 17           | 57 mm² ± 11            | <0.0001*                          |
|                                                                           | Male   | 122 mm² ± 20           | 61 mm² ± 15            | <0.0001*                          |
| Whole indirect insertion area                                            | Female | 19 mm² ± 6             | 47 mm² ± 14            | <0.0001*                          |
|                                                                           | Male   | 17 mm² ± 4             | 56 mm² ± 15            | <0.0001*                          |
| Whole AM footprint area                                                   | Female | 67 mm² ± 15            | 55 mm² ± 13            | n.s.                              |
|                                                                           | Male   | 78 mm² ± 13            | 62 mm² ± 14            | n.s.                              |
| Direct insertion area of AM bundle                                       | Female | 52 mm² ± 10            | 26 mm² ± 7             | <0.0001*                          |
|                                                                           | Male   | 63 mm² ± 11            | 32 mm² ± 8             | <0.0001*                          |
| Indirect insertion area of AM bundle                                     | Female | 10 mm² ± 3             | 25 mm² ± 5             | <0.0001*                          |
|                                                                           | Male   | 12 mm² ± 3             | 34 mm² ± 8             | <0.0001*                          |
| Whole PL footprint area                                                   | Female | 59 mm² ± 10            | 53 mm² ± 8             | n.s.                              |
|                                                                           | Male   | 65 mm² ± 11            | 58 mm² ± 9             | n.s.                              |
| Direct insertion area of PL bundle                                       | Female | 48 mm² ± 5             | 24 mm² ± 3             | <0.0001*                          |
|                                                                           | Male   | 51 mm² ± 6             | 29 mm² ± 5             | <0.0001*                          |
| Indirect insertion area of PL bundle                                     | Female | 10 mm² ± 1             | 22 mm² ± 5             | <0.0001*                          |
|                                                                           | Male   | 12 mm² ± 2             | 28 mm² ± 7             | <0.0001*                          |
given that an anterior border straight and a posterior border convex have been described. Conversely, most authors have described an ovoid or elliptical insertion area [3, 18, 19, 21, 26, 34, 35, 38]. All those studies were conducted on cadavers of people with a mean age that was greater than 50 years. Thus, more studies on the cadavers of younger people need to be done to confirm the observed morphology.

Due to the decrease in the size of the direct insertion with increasing age, the mean distance from the insertion of the ACL to the posterior cartilage of the lateral femoral condyle increases from 2.3 to 8.2 mm ($p < 0.0001$) in women, and from 2.1 to 7.9 mm in men ($p < 0.0001$). On the contrary, the morphometries towards the lower and anterior cartilage do not suffer significant changes. In this study, the direct insertion of the ACL decreases at its anteroposterior axis, which causes this structure to become thinner or flattened in patients older than 50, similar to previous studies [37, 39].

On the other hand, the difference between the different age groups in the areas corresponding to the direct and indirect insertions of the ACL is great. We hypothesize that this indirect insertion occurs as a consequence of the degeneration of the fibers of direct insertion of the ACL that this indirect insertion occurs as a consequence of the indirect insertions of the ACL is great. We hypothesize that the morphometries towards the lower and anterior cartilage do not suffer significant changes. In this study, the direct insertion of the ACL decreases at its anteroposterior axis, which causes this structure to become thinner or flattened in patients older than 50, similar to previous studies [37, 39].

Here, a significant increase in the indirect insertion area was observed in patients over 50 years of age, presenting 50 mm$^2$ (SD ± 14) in women and 56 mm$^2$ (SD ± 15) in men, similar to that observed in previous studies. Suruga et al. reported an area of 59 mm$^2$ in patients with a mean age of 83 years [39], and Iriuchishima et al. reported 45 mm$^2$ with a mean age of 82.5 years [16]. In addition, it was observed that indirect fibers have a smaller insertional area in the cadavers of those under 50 years of age when compared to the over-50 cadavers, showing that indirect fibers increase with age. This effect may be due to a degeneration of the direct fibers into fan-like fibers as age increases.

There are previous studies that showed degenerative histopathologic changes in the ACL bundles that occur with aging in osteoarthritic knees, presenting a weaker and thinner ligament in those patients [4, 14, 28] that may explain the degeneration of the mid substance insertions on the femoral condyle. A recent study demonstrated that both fascicles of the ACL presented histologic changes. The AM bundle showed degenerative changes in 53% of the specimens and the PL bundle showed degeneration in 78% of the knees. The PL fascicle also presented more severe degenerative changes [41], suggesting that intercondylar notch stenosis and intercondylar notch osteophytes led to ACL destruction [15, 22].

For this reason, describing the correct size and morphology of the ACL footprint is critical to reproducing the native anatomy as closely as possible. It is important to consider this change in the configuration of the ACL morphology as age advances for carrying out femoral tunnels in ACL reconstruction. Subsequent studies with cadavers divided into decadal subgroups, for example, are needed to confirm our results [5, 30].

These findings should be considered to avoid employing reconstruction techniques in which femoral tunnels with oval
Conclusions

The femoral insertion of the ACL presents variations in its morphology, area and morphometric characteristics over time. It goes from a large semicircular shape that almost contacts the posterior articular cartilage in the younger group to a smaller, flattened and ribbon-like shape that moves away from the edge of the articular cartilage and is kept in bound anteriorly by the lateral intercondylar ridge in the older age group.

Acknowledgements The authors would like to thank all the technical staff of the Macroscopic Anatomy Laboratory of the Department of Human Anatomy of the U.A.N.L. School of Medicine. Also to Mr. Eric Goode for his help in reviewing the English language.

Author contributions RMA; conception of the research idea, protocol design and drafting, obtaining, analyzing and interpreting the data, drafting the manuscript and approval of its final version, search for current and ancient literature as well as an agreement that all of the manuscript's minors were reviewed and it has validity and integrity. VMPM; intellectual contribution and revision of the manuscript from the orthopedic point of view, methodological support for the design of the study, acquisition, analysis and interpretation of the data, writing of part of the manuscript, approval of the final version of the manuscript, realization of the covenants for the obtaining cadaveric samples, reviewer of the entire manuscript. SGL; substantial contribution to the manuscript from the anatomical point of view, proposal of the research idea, contribution of cadaver for the study, approval of the final version of the manuscript interpretation of the data, supervision of the study. REEO; substantial contribution to the manuscript from the anatomical point of view, proposal of the research idea, contribution of cadaver for the study, approval of the final version of the manuscript interpretation of the data, supervision of the study. JRPM; conception of the research idea, protocol design and drafting, obtaining, analyzing and interpreting the data, carrying out the dissections, drafting the manuscript, approval of the final version, JCM; one of the two main investigators of the study, editing of the manuscript before its final version, orthopedic adviser, proposal of the idea, proposal of the clinical relevance of the study, implementation of the protocol methodology, interpretation of results, approval of the final version, writing of part of the manuscript.

Funding Open Access Funding provided by Universitat Autonoma de Barcelona. None.

Declarations

Conflict of interest Each author certifies that neither he or she, nor any member of his or her immediate family, has funding or commercial associations (consultancies, stock ownership, equity interest, patent/ licensing arrangements, etc.) that might pose a conflict of interest in connection with the submitted article. Each author certifies that his or her institution approved the human protocol for this investigation and that all investigations were conducted in conformity with ethical principles of research.

Ethical approval The present protocol was approved by the Institutional review board of the Faculty of Medicine and University Hospital Dr. José Eleuterio Gonzalez of the Universidad Autonoma de Nuevo Leon (OR16-00007).

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article’s Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/.

References

1. Araki D, Thorhauer E, Tashman S (2018) Three-dimensional isotropic magnetic resonance imaging can provide a reliable estimate
of the native anterior cruciate ligament insertion site anatomy. Knee Surg Sports Traumatol Arthrosc 26:1311–1318
2. Benkhadra M, Bouchot A, Gérard J, Genelot D, Trouilloud P, Martin L, Girard C, Danino A, Anderhuber F, Feigl G (2011) Flexibility of Thiel’s embalmed cadavers: the explanation is probably in the muscles. Surg Radiol Anat 33:365–368
3. Colombet P, Robinson J, Christel P, Franceschi JP, Dijan P, Bellier G, Shibib A (2006) Morphology of anterior cruciate ligament attachments for anatomic reconstruction: a cadaveric dissection and radiographic study. Arthroscopy 22:984–992
4. Cusner FD, La Rosa DF, Vigorita VJ, Scuderi GR, Scott WN, Insall JN (2003) A quantitative histologic comparison: ACL degeneration in the osteoarthritic knee. J Arthroplasty 18:687–692
5. Dhawan A, Gallo RA, Lynch SA (2016) Anatomic tunnel placement in anterior cruciate ligament reconstruction. J Am Acad Orthop Surg 24:443–454
6. Duffee A, Magnussen RA, Pedroza AD, Flanigan DC, Kaeding CC (2013) Transstibial ACL femoral tunnel preparation increases odds of repeat ipsilateral knee surgery. J Bone Jt Surg Am 95:2035–2042
7. Ferrecci M, Ekdahl M, Shen W, Fu FH (2007) Osseous landmarks of the femoral attachment of the anterior cruciate ligament: an anatomic study. Arthroscopy 23:1218–1225
8. Fujimaki Y, Thorhauer E, Sasaki Y, Smolinski P, Tashman S, Fu FH (2016) Quantitative in situ analysis of the anterior cruciate ligament. Am J Sports Med 44:118–125
9. Gali JC, Camargo DB, de Oliveira FAM, Pereira RHN, da Silva PAC (2018) Descriptive anatomy of the anterior cruciate ligament femoral insertion. Rev Bras Ortop 53:421–426
10. Girgis FG, Marshall JL, Monajem A (1975) The cruciate ligaments of the knee joint. Anatomical, functional and experimental analysis. Clin Orthop Relat Res 106:216–231
11. Hara K, Mochizuki T, Sekiya I, Yamaguchi K, Akita K, Muneta T (2009) Anatomy of normal human anterior cruciate ligament attachments evaluated by divided small bundles. Am J Sports Med 37:2386–2391
12. Harner CD, Baek GH, Vogrin TM, Carlin GJ, Kashiwaguchi S, Woo SLY (1999) Quantitative analysis of human cruciate ligament insertions. Arthroscopy 15:741–749
13. Hart A, Han Y, Martineau PA (2015) The apex of the deep cartilage: a landmark and new technique to help identify femoral tunnel placement in anterior cruciate ligament reconstruction. Arthroscopy 31:1777–1783
14. Hasegawa A, Otsubo H, Suzuki T, Amano H, Nakamura N (2010) Direct anterior cruciate ligament insertion to the femur assessed by histology and 3-dimensional volume-rendered computed tomography. Arthroscopy 26:S13–S20
15. Iwama G, Iriuchishima T, Horaguchi T, Aizawa S (2019) Measurement of the whole and midsubstance femoral insertion of the anterior cruciate ligament: the comparison with the elliptically calculated femoral anterior cruciate ligament footprint area. Indian J Orthop 53:727–731
16. Kim Y-M, Joo Y-B, Lee K-Y, Hwang SJ (2018) Femoral footprint for anatomical single-bundle anterior cruciate ligament reconstruction: a cadaveric study. Knee Surg Relat Res 30:128–132
17. Lalwani R, Srivastava R, Kotgirwar S, Athavale SA (2020) New insights in anterior cruciate ligament morphology: implications for anterior cruciate ligament reconstruction surgeries. Anat Cell Biol 53:398–404
18. León HO, Blanco CER, Guthrie TB, Martínez OJN (2005) Intercondylar notch stenosis in degenerative arthritis of the knee. Arthroscopy 21:294–302
19. Loh JC, Fukuda Y, Tsuda E, Steadman RJ, Fu FH, Woo SLY (2003) Knee stability and graft function following anterior cruciate ligament reconstruction: comparison between 11 o’clock and 10 o’clock femoral tunnel placement. 2002 Richard O’Connor Award paper. Arthroscopy 19:297–304
20. Matassi F, Sirleò L, Carulli C, Innocenti M (2015) Anatomical anterior cruciate ligament reconstruction: transtibial versus outside-in technique: SIGASCOT Best Paper Award Finalist 2014. Joints 3:6–14
21. Mochizuki T, Fujishiro H, Nimura A, Mahakkanukrauh P, Yasuda K, Muneta T, Akita K (2014) Anatomical and histologic analysis of the mid-substance and fan-like extension fibres of the anterior cruciate ligament during knee motion, with special reference to the femoral attachment. Knee Surg Sports Traumatol Arthrosc 22:336–344
22. Moreiras-Avalos R, Castillo-Escobedo TA, Elizondo-Omaña RE, del Carmen T-G, Perelli S, Guzmán-López S, Peña-Martínez VM, Vilchez-Cavazos F, Monlau JC (2021) The morphology of the tibial footprint of the anterior cruciate ligament changes with ageing from oval/elliptical to C-shaped. Knee Surg Sports Traumatol Arthrosc 29:922–930
23. Mullaji AB, Mararaw SV, Simha M, Jindal G (2008) Cruciate ligaments in arthritic knees: a histologic study with radiologic correlation. J Arthroplasty 23:567–572
24. Odensten M, Gillquist J (1985) Functional anatomy of the anterior cruciate ligament and a rationale for reconstruction. J Bone Jt Surg Am 67:257–262
25. Parkar AP, Adriaensen ME, Vindfeld S, Solheim E (2017) The anatomic centers of the femoral and tibial insertions of the anterior cruciate ligament: a systematic review of imaging and cadaveric studies reporting normal center locations. Am J Sports Med 45:2180–2188
26. Petersen W, Tillmann B (2002) Anatomy and function of the anterior cruciate ligament. Orthopade 31:710–718
27. Rahnevai-Azar AA, Sabzevari S, Irrazával S, Chao T, Fu FH (2016) Anatomical individualized ACL reconstruction. Arch Bone Jt Surg 4:291–297
28. Sabzevari S, Shaikh H, Marshall B, Zhu J, Linde MA, Smolinski P, Fu FH (2020) The femoral posterior fan-like extension of the ACL insertion increases the failure load. Knee Surg Sports Traumatol Arthrosc 28:1113–1118
29. Sasaki N, Ishibashi Y, Tsuda E, Shirasawa S, Akita S, Sekiya I (2006) Cadaveric knee observation study for describing anatomical femoral tunnel placement for two-bundle anterior cruciate ligament reconstruction. Arthroscopy 22:356–361
30. Vílchez-Cavazos F, Monllau JC (2021) The morphology of the femoral anterior cruciate ligament: a systematic review of imaging and cadaveric studies reporting normal center locations. Am J Sports Med 45:2180–2188
31. Petersen W, Tillmann B (2002) Anatomy and function of the anterior cruciate ligament. Orthopade 31:710–718
32. Rahnevai-Azar AA, Sabzevari S, Irrazával S, Chao T, Fu FH (2016) Anatomical individualized ACL reconstruction. Arch Bone Jt Surg 4:291–297
33. Sabzevari S, Shaikh H, Marshall B, Zhu J, Linde MA, Smolinski P, Fu FH (2020) The femoral posterior fan-like extension of the ACL insertion increases the failure load. Knee Surg Sports Traumatol Arthrosc 28:1113–1118
34. Sasaki N, Ishibashi Y, Tsuda E, Yamamoto Y, Maeda S, Mizukami H, Toh S, Yagihashi S, Tonosaki Y (2012) The femoral insertion of the anterior cruciate ligament: discrepancy between macroscopic and histological observations. Arthroscopy 28:1135–1146
35. Scheffler SU, Maschewski K, Becker R, Asbach P (2018) In vivo three-dimensional MR imaging of the intact anterior cruciate ligament.
cruciate ligament shows a variable insertion pattern of the femoral and tibial footprints. Knee Surg Sports Traumatol Arthroscopy 26:3667–3672
36. Siebold R, Ellert T, Metz S, Metz J (2008) Femoral insertions of the anteromedial and posterolateral bundles of the anterior cruciate ligament: morphometry and arthroscopic orientation models for double-bundle bone tunnel placement—a cadaver study. Arthroscopy 24:585–592
37. Śmigielski R, Zdanowicz U, Drwięga M, Ciszek B, Ciszkowska-Lysoń B, Siebold R (2015) Ribbon like appearance of the midsubstance fibres of the anterior cruciate ligament close to its femoral insertion site: a cadaveric study including 111 knees. Knee Surg Sports Traumatol Arthroscopy 23:3143–3150
38. Suruga M, Horaguchi T, Iriuchishima T, Iwama G, Yahagi Y, Tokuhashi Y, Aizawa S (2019) The correlation between the femoral anterior cruciate ligament footprint area and the morphology of the distal femur: three-dimensional CT evaluation in cadaveric knees. Eur J Orthop Surg Traumatol 29:849–854
39. Suruga M, Horaguchi T, Iriuchishima T, Yahagi Y, Iwama G, Tokuhashi Y, Aizawa S (2017) Morphological size evaluation of the mid-substance insertion areas and the fan-like extension fibers in the femoral ACL footprint. Arch Orthop Trauma Surg 137:1107–1113
40. Takahashi M, Doi M, Abe M, Suzuki D, Nagano A (2006) Anatomical study of the femoral and tibial insertions of the anteromedial and posterolateral bundles of human anterior cruciate ligament. Am J Sports Med 34:787–792
41. Tampere T, Van Hoof T, Cromheecke M, Van der Bracht H, Chahla J, Verdonk P, Victor J (2017) The anterior cruciate ligament: a study on its bony and soft tissue anatomy using novel 3D CT technology. Knee Surg Sports Traumatol Arthroscopy 25:236–244
42. Van Eck CF, Lesniak BP, Schreiber VM, Fu FH (2010) Anatomic single- and double-bundle anterior cruciate ligament reconstruction flowchart. Arthroscopy 26:258–268
43. Watanabe A, Kanamori A, Ikeda K, Ochiai N (2011) Histological evaluation and comparison of the anteromedial and posterolateral bundle of the human anterior cruciate ligament of the osteoarthritic knee joint. Knee 18:47–50
44. Zantop T, Petersen W, Sekiya JK, Musahl V, Fu FH (2006) Anterior cruciate ligament anatomy and function relating to anatomical reconstruction. Knee Surg Sports Traumatol Arthroscopy 14:982–992
45. World Medical Association (2013) World Medical Association Declaration of Helsinki: ethical principles for medical research involving human subjects. JAMA 310:2191–2194

Publisher’s Note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.