Alterations in intrinsic functional networks in Parkinson’s disease patients with depression: A resting-state functional magnetic resonance imaging study

Yi-Hui Qiu1 | Zhi-Heng Huang1 | Yu-Yuan Gao1 | Shu-Jun Feng1 | Biao Huang2 | Wan-Yi Wang1 | Qi-Huan Xu1 | Jie-Hao Zhao1 | Yu-Hu Zhang1 | Li-Min Wang1 | Kun Nie1 | Li-Juan Wang1

1Department of Neurology, Guangdong Provincial Peoples’ Hospital, Guangdong Academy of Medical Sciences, Guangdong Neuroscience Institute, Guangzhou, China
2Department of Radiology, Guangdong Provincial Peoples’ Hospital, Guangdong Academy of Medical Sciences, Guangzhou, China

Abstract

Aims: The aim of this research was to investigate the alterations in functional brain networks and to assess the relationship between depressive impairment and topological network changes in Parkinson’s disease (PD) patients with depression (DPD).

Methods: Twenty-two DPD patients, 23 PD patients without depression (NPD), and 25 matched healthy controls (HCs) were enrolled. All participants were examined by resting-state functional magnetic resonance imaging scans. Graph theoretical analysis and network-based statistic methods were used to analyze brain network topological properties and abnormal subnetworks, respectively.

Results: The DPD group showed significantly decreased local efficiency compared with the HC group (P = .008, FDR corrected). In nodal metrics analyses, the degree of the right inferior occipital gyrus (P = .0001, FDR corrected) was positively correlated with the Hamilton Depression Rating Scale scores in the DPD group. Meanwhile, the temporal visual cortex, including the bilateral middle temporal gyri and right inferior temporal gyrus in the HC and NPD groups and the left posterior cingulate gyrus in the NPD group, was defined as hub region, but not in the DPD group. Compared with the HC group, the DPD group had extensive weakening of connections between the temporal-occipital visual cortex and the prefrontal-limbic network.

Conclusions: These results suggest that PD depression is associated with disruptions in the topological organization of functional brain networks, mainly involved the temporal-occipital visual cortex and the posterior cingulate gyrus and may advance our current understanding of the pathophysiological mechanisms underlying DPD.

Key Words
depression, functional magnetic resonance imaging, graph theory, network-based statistical analysis, Parkinson’s disease

Qiu and Huang are contributed equally to this work.

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INTRODUCTION

Parkinson’s disease (PD) is a common neurodegenerative disease with a growing incidence in recent decades. Depression is considered one of the most common nonmotor symptoms of PD, with an incidence of up to 40%. In addition, depression is one of the established clinical prodromal markers and may be an independent risk factor for PD, often occurring before motor symptoms appear and causing a serious negative impact on PD patients’ quality of life. However, the pathophysiology underlying the contribution of depression to PD remains unclear. Thus, exploring the pathological mechanisms of depression in PD may contribute to early identification and effective treatment of PD patients in the clinical prodromal stage of the disease; that is, it might delay the progression of the disease and improve quality of life.

With the rapid development of imaging technology and its continuous application in neuroscience research, strong noninvasive technical support is available for exploring the pathogenesis of neuropsychiatric diseases and realizing the early diagnosis of PD patients with depression (DPD). Graph theory provides a powerful mathematical framework for describing the topological organization of brain networks in terms of nodes (ie, brain regions) and edges (ie, physical or functional connections between brain regions). The latest research has suggested that network topological metric measurements derived using graph theory may be potential biomarkers in PD to evaluate disease progression and to monitor therapeutic effects. By using diffusion tensor imaging, one study showed that despite preserved small-world topology, DPD exhibited higher network efficiency in the fronto-limbic system compared to that in PD patients without depression (NDPD). Gou et al, by using graph theory and network-based statistic (NBS) methods, showed that the integration of the structural brain network was impaired with disrupted connectivity of the limbic and visual systems in de novo and drug-naïve DPD patients. Notably, these results were approximately consistent with those obtained from depressive patients, suggesting that deficits of the regional and connectivity characteristics in the structural networks were primarily found in the frontal brain regions, limbic system, and occipital lobe compared to that in healthy controls (HCs). Therefore, it is an urgent problem to explore the characteristic imaging markers of DPD and to realize early diagnosis and treatment. A previous study showed that even though the overall structural organization of the PD connectome remains robust at relatively early disease stages, there is a breakdown in the functional modular organization of the PD connectome. Therefore, characterization of the functional network connectome in DPD patients may help researchers to further explore the mechanisms underlying DPD.

The purpose of this study was to investigate the changes in the topological properties and the functional connectivity of the whole-brain functional network in patients with DPD and to assess whether depressive impairment is correlated with functional topological network changes in DPD patients.

MATERIALS AND METHODS

Participants

Forty-five patients with idiopathic PD and 27 age-, sex-, and years of education–matched HCs were enrolled from the Department of Neurology at Guangdong Provincial Peoples’ Hospital in China. PD was diagnosed according to the Movement Disorder Society (MDS) Clinical Diagnostic Criteria for PD. Twenty-two PD patients were diagnosed with depressive disorder according to the Diagnostic and Statistical Manual of Mental Disorders, 5th edition (DSM-V) criteria, and the remaining twenty-three patients had PD alone. None of the patients had used any antidepressant(s). Individuals with Parkinson’s plus syndrome (PPS) caused by vascular factors, toxins, drugs, etc, were excluded. Participants were also excluded if they had dementia, other severe neuropsychiatric disorders, or serious respiratory, cardiovascular, and digestive diseases. All participants were right-handed. This study was approved by the Research Ethics Committee of Guangdong Provincial People’s Hospital, Guangdong Academy of Medical Sciences. All participants provided written informed consent prior to their inclusion in the study.

Neuropsychological assessments

Motor symptom severity in PD patients was measured by the MDS Unified PD Rating Scale (MDS-UPDRS) part III and the Hoehn and Yahr (H&Y) scale. All participants were screened for depression, anxiety, and cognitive function using the Hamilton Depression Rating Scale (HAMD), Hamilton Anxiety Rating Scale (HAMA), and Mini-Mental State Examination (MMSE), respectively. The levodopa equivalent dose (LED) was calculated for each PD patient.

MRI data acquisition

All the PD subjects in this study underwent rs-fMRI after discontinuing antiparkinsonian medication for more than 12 hours. The scans were performed on a 3.0T GE SIGNA MR scanner (Signa Excite HD; GE Healthcare) with an 8-channel head coil in the Department of Radiology of Guangdong Provincial People’s Hospital. All participants were required to keep their eyes closed, relax, and remain awake during the MRI scans. The rs-fMRI scanning parameters were as follows: a gradient-echo echo-planar imaging (GRE-EPI) sequence with a repetition time (TR)/echo time (TE) = 2000/30 ms, matrix = 64 x 64, 30 axial slices covering the entire brain, field of view = 240 x 240 mm, slice thickness = 4 mm, interslice space = 1 mm, NEX = 1, voxel size = 3.75 mm x 3.75 mm x 4 mm, and time points = 186. Axial scans were parallel to the anterior-posterior commissure (AC-PC) line. High-resolution 3D T1-weighted anatomical images were obtained for coregistration with the functional data. A fast spoiled gradient recalled echo inversion recovery sequence was used to acquire sagittal T1-weighted images with the following parameters: TR/
TE = 8.4/3.3 ms, matrix = 256 × 256, flip angle = 13°, slice thickness = 1 mm, and voxel size = 0.94 mm × 0.94 mm × 1 mm.

### 2.4 Data preprocessing

Data preprocessing was performed on the MATLAB-based DPABI, the Data Processing Assistant for rs-fMRI. The first ten volumes of the functional images were discarded. The remaining volumes were slice-time corrected, and realignment was performed to correct the motion between time points. Head motion parameters were computed by estimating the translation in each direction and the angular rotation on each axis for each volume. The subjects with motion (a mean framewise displacement [FD] Jenkinson) greater than 2 standard deviations (SDs) above the group mean motion were excluded. According to this exclusion criterion, only two subjects were excluded from the HC group (Tables S1 and S2). No significant intergroup differences were found in head motion (Table 1). The fMRI data were coregistered to the same subject’s high-resolution T1-weighted image. The coregistered images were segmented into gray matter, white matter (WM), and cerebrospinal fluid (CSF) and were then spatially normalized to the standard stereotaxic coordinates of the Montreal Neurological Institute space using an echenplanar imaging template and resampled into a voxel size of 3 × 3 × 3 mm. Then, WM, CSF, and head motion were removed as nuisance variables; head motion was removed using the Friston 24-parameter model. The generated images were spatially smoothed with a 4-mm full-width at half-maximum Gaussian kernel. A temporal filter (0.01-0.1 Hz) was used to decrease the effect of low-frequency drifts and physiological high-frequency noise. In addition, adequate quality control was conducted on MRI data, which is essential for establishing reliable results.

### 2.5 Brain network construction

The binarized functional brain network was constructed by GRENTA, a graph theoretical network analysis toolbox for imaging connectomics. The functional connectivity matrices (composed of positive correlations), which were used to analyze brain

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**TABLE 1** Demographic and clinical characteristics and global topological properties of the NDPD, DPD, and HC groups

| Measure                  | NDPD     | DPD      | HCs     | F/H/χ²/Z | P-value | P-value (NDPD vs HCs) | P-value (DPD vs HCs) | P-value (DPD vs NDPD) |
|-------------------------|----------|----------|---------|----------|---------|----------------------|----------------------|----------------------|
| Sex (male/female)       | 16/7     | 13/9     | 9/16    |          |         |                      |                      |                      |
| Age                     | 66.00 (23.00) | 64.50 (17.00) | 55.00 (11.50) | 5.737    | 0.057   |                      |                      |                      |
| Education (y)           | 10.09 ± 4.842 | 9.50 ± 4.718 | 8.80 ± 3.764 | 1.273    | 0.529   |                      |                      |                      |
| Course of the disease (y)| 3.00 (4.50) | 3.00 (4.50) | NA      | -0.820   | 0.412   |                      |                      |                      |
| LED                     | 0.00 (0.00, 275.00) | 0.00 (0.00, 505.00) | NA      | -1.269   | 0.204   |                      |                      |                      |
| H&Y Stage               | 2.00 (1.00) | 2.00 (1.50) | NA      | -0.074   | 0.941   |                      |                      |                      |
| MDS-UPDRS-III           | 35.00 (9.00) | 39.00 (17.25) | NA      | -1.957   | 0.050   |                      |                      |                      |
| MMSE                    | 28.00 (2.00) | 28.00 (3.00) | 27.50 (4.00) | 0.973    | 0.615   |                      |                      |                      |
| HAMD                    | 7.00 (4.00) | 22.50 (9.25) | 1.00 (3.50) | 53.621   | <0.001  | 0.009                | <0.001               | <0.001               |
| HAMA                    | 6.00 (4.00) | 18.00 (11.50) | 2.00 (2.00) | 49.093   | <0.001  | 0.014                | <0.001               | <0.001               |
| Mean F/Jenkinson        | 0.067 (0.037) | 0.054 (0.091) | 0.065 (0.055) | 0.068    | 0.967   |                      |                      |                      |
| Eglob                   | 0.260 ± 0.005 | 0.257 ± 0.009 | 0.258 ± 0.008 | 0.883    | 0.418   |                      |                      |                      |
| Elc                     | 0.345 ± 0.012 | 0.341 ± 0.011 | 0.348 ± 0.008 | 3.230    | 0.046   | 0.193                | 0.008                | 0.266                |
| Modularity              | 0.143 ± 0.017 | 0.140 ± 0.018 | 0.141 ± 0.021 | 0.115    | 0.892   |                      |                      |                      |
| Lp                      | 0.842 ± 0.031 | 0.858 ± 0.047 | 0.862 ± 0.070 | 0.917    | 0.405   |                      |                      |                      |
| Cp                      | 0.271 ± 0.019 | 0.267 ± 0.020 | 0.278 ± 0.011 | 2.437    | 0.095   |                      |                      |                      |
| λ                       | 0.487 ± 0.012 | 0.491 ± 0.016 | 0.494 ± 0.017 | 1.394    | 0.255   |                      |                      |                      |
| γ                       | 0.868 ± 0.098 | 0.858 ± 0.113 | 0.901 ± 0.154 | 0.765    | 0.469   |                      |                      |                      |
| σ                       | 0.778 ± 0.084 | 0.765 ± 0.102 | 0.796 ± 0.137 | 0.491    | 0.614   |                      |                      |                      |

Abbreviations: Cp, the clustering coefficient; DPD, Parkinson’s disease patients with depression; Eglob, the global efficiency; Elc, the local efficiency; H&Y, Hoehn and Yahr scale; HAMA, Hamilton Anxiety Rating Scale; HAMD, Hamilton Depression Rating Scale; HCs, healthy controls; LED, levodopa equivalent dose; Lp, the characteristic path length; MDS-UPDRS-III, MDS Unified Parkinson’s Disease Rating Scale (MDS-UPDRS) part III; MMSE, Mini-Mental State Examination; NA, not applicable; NDPD, Parkinson’s disease patients without depression; γ, the normalized clustering coefficient; λ, the normalized characteristic path length; σ, small worldness.
network topological properties and to examine abnormal subnetworks, were constructed in two major steps: network node definition and network edge definition. The atlas of automated anatomical labeling (AAL) was employed to parcellate the entire brain into 90 (45 for each hemisphere) cortical and subcortical regions of interest (Table 2), with each representing a node of the network. Pearson’s correlation coefficients for each pair of regions were computed for the mean time series for each of the 90 regions and defined as the edge of the network. Then, Fisher’s transformation was performed to transform the data into z-values that were close to normally distributed. Sparsity (Sp) was employed as the threshold metric to compute the network properties, with a range of 0.05–0.50 and a step length of 0.01. Sparsity is defined as the ratio of the number of actual edges divided by the maximum possible number of edges in a network. For networks with the same number of nodes, the sparsity threshold ensures the same number of edges for each network by applying a subject-specific connectivity strength threshold and therefore allowing examination of the relative network organization.

| Number | Region | Abbreviations |
|--------|--------|---------------|
| 1, 2   | Precentral gyrus | PreCG |
| 3, 4   | Superior frontal gyrus, dorsolateral | SFGdor |
| 5, 6   | Superior frontal gyrus, orbital part | ORBsup |
| 7, 8   | Middle frontal gyrus | MFG |
| 9, 10  | Middle frontal gyrus, orbital part | ORBmid |
| 11, 12 | Inferior frontal gyrus, opercular part | IFGoperc |
| 13, 14 | Inferior frontal gyrus, triangular part | IFGtriang |
| 15, 16 | Inferior frontal gyrus, orbital part | ORBinf |
| 17, 18 | Rolandic operculum | ROL |
| 19, 20 | Supplementary motor area | SMA |
| 21, 22 | Olfactory cortex | OLF |
| 23, 24 | Superior frontal gyrus, medial | SFGmed |
| 25, 26 | Superior frontal gyrus, medial orbital | ORBMed |
| 27, 28 | Gyrus rectus | REC |
| 29, 30 | Insula | INS |
| 31, 32 | Anterior cingulate and paracingulate gyri | ACG |
| 33, 34 | Median cingulate and paracingulate gyri | MCG |
| 35, 36 | Posterior cingulate gyrus | PCG |
| 37, 38 | Hippocampus | HIP |
| 39, 40 | Para hippocampal gyrus | PHG |
| 41, 42 | Amygdala | AMYG |
| 43, 44 | Calcarine fissure and surrounding cortex | CAL |
| 45, 46 | Cuneus | CUN |
| 47, 48 | Lingual gyrus | LING |
| 49, 50 | Superior occipital gyrus | SOG |
| 51, 52 | Middle occipital gyrus | MOG |
| 53, 54 | Inferior occipital gyrus | IOG |
| 55, 56 | Fusiform gyrus | FFG |
| 57, 58 | Postcentral gyrus | PoCG |
| 59, 60 | Superior parietal gyrus | SPG |
| 61, 62 | Inferior parietal lobule | IPL |
| 63, 64 | Supramarginal gyrus | SMG |
| 65, 66 | Angular gyrus | ANG |
| 67, 68 | Precuneus | PCUN |
| 69, 70 | Paracentral lobule | PCL |
| 71, 72 | Caudate | CAU |
| 73, 74 | Putamen | PUT |
| 75, 76 | Pallidum | PAL |
| 77, 78 | Thalamus | THA |
| 79, 80 | Heschl gyrus | HES |
| 81, 82 | Superior temporal gyrus | STG |

(Continues)
2.7 Statistical analysis

All analyses of demographic and clinical characteristics were performed using SPSS Statistics 22.0. The $\chi^2$ test was used to analyze the sex ratios among the three groups. One-way analysis of variance (ANOVA) was used for education years, and a pairwise post hoc test was subsequently used to identify significant main group differences with correction by the Bonferroni test. Age and MMSE, HAMD, and HAMA scores were compared by the Kruskal-Wallis H test and further evaluated by post hoc tests (Bonferroni’s test). The Mann-Whitney U test was used to compare the LED, H&Y stage, and MDS-UPDRS-III scores between the DPD and NDPD groups. The statistical significance threshold was set at $P < .05$.

The imaging data were analyzed based on a general linear model (GLM) on GRETNA. ANOVA was used to compare the AUCs of network topological properties among the three groups. Post hoc analyses were performed using two-sample $t$ tests in a pairwise manner within the areas identified by the ANOVA. With age, years of education, disease course, the LED, H&Y stage, and MDS-UPDRS-III, MMSE, and HAMA scores as covariates, correlation analysis was used to test correlations between network topological properties and HAMD scores in the DPD group. To address the problem of multiple comparisons in the nodal metrics, a false discovery rate (FDR) $q$ of 0.05 multiple comparisons correction was performed.

Next, to determine the significance levels of altered connectivity networks in NBS analysis, we first performed two-sample $t$ test at each edge independently to test for significant differences in the value of connectivity between two groups. A primary component-forming threshold ($P = .05$) was then applied to form a set of suprathreshold edges among which any connected components and their size could then be determined. Next, the statistical significance of the size of each observed component was then evaluated with respect to an empirical null distribution of maximal component sizes obtained under the null hypothesis of random group membership (50,000 permutations). Subnetworks that were significant at a corrected level of $P = .001$ were reported. The effects of age, gender, and years of education were adjusted for these analyses.

3 RESULTS

3.1 Population characteristics

The demographic and clinical features of the participants are presented in Table 1. No significant differences were observed in age, sex, years of education, or MMSE scores among the three groups. In addition, the DPD and NDPD patients had comparable values for disease course, the LED, H&Y stage, and MDS-UPDRS-III scores. However, both the HAMD and HAMA scores in the DPD group were significantly higher than those in the other two groups ($P < .001$), which is consistent with previous studies revealing that DPD coexisted with anxiety disorder.

3.2 Global network analyses

Over the sparsity range of 0.05-0.50 (step = 0.01), the DPD, NDPD, and HC groups exhibited a high-efficiency small-world topology ($\gamma = C_p/C_r > 1$, $\lambda = L_p/L_r \approx 1$ and $\sigma = \gamma/\lambda > 1$; Figure 1).

Statistical comparisons were performed to detect significant differences in the AUCs of global parameters among the three groups. The DPD group showed a significantly lower integrated $E_{loc}$ ($P = .008$, FDR corrected) compared with the HC group. No significant differences ($P > .05$) were found in $E_{glob}$, $L_p$, $C_p$, modularity, $\gamma$, $\lambda$, and $\sigma$ (Table 1).

![Figure 1](https://example.com) The results of small-world properties of the three groups of subjects under different sparsity. Bars and error bars represent mean values and standard deviation, respectively. $\gamma$, the normalized characteristic path length; $\lambda$, the normalized clustering coefficient; $\sigma$, small worldness; DPD, Parkinson’s disease patients with depression; NDPD, Parkinson’s disease patients without depression; HCs, healthy controls [Colour figure can be viewed at wileyonlinelibrary.com]
3.3 | Regional network analyses

3.3.1 | Intergroup differences in local topological properties

Brain regions exhibiting significant intergroup differences in at least one nodal metric (the degree, efficiency, or betweenness) were identified. But there were no brain regions surviving the FDR correction for multiple comparisons.

3.3.2 | Differences in hub regions among the three groups

The hubs were identified as nodes with both degree and betweenness centrality that were one SD above the network averages. In the HC group, five hub regions were defined in the temporal visual area, including the bilateral fusiform gyri (FFG), bilateral middle temporal gyri (MTG), and right inferior temporal gyrus (ITG.R). Compared with the HC group, the NDPD group lacked the bilateral FFG as hub regions, while the left posterior cingulate gyrus (PCG.L) was a hub region. However, no hub regions were screened out in the DPD group (Tables 3 and S5).

3.4 | Correlations between network topological properties and HAMD scores in the DPD group

Figure 2 and Table S3 present the results of the correlation analysis between the degree and HAMD scores in the DPD group. A significantly and specifically positive correlation was observed in the right inferior occipital gyrus (IOG.R; $r = .848$, $P = .0001$, FDR corrected) that was not present in the NDPD group (Table S4). There was no correlation between HAMD scores and the other network topological properties surviving the FDR correction for multiple comparisons.

3.5 | Functional connectivity characteristics

In the NBS analysis, the primary test statistic thresholds were set to 3.521 (DPD vs HCs), 3.533 (NDPD vs HCs), and 2.019 (DPD vs NDPD) according to the test results. One subnetwork consisting of seven nodes and eight edges with decreased functional connectivity was characterized in the NDPD group compared with the HC group, including the left inferior frontal gyrus, opercular part (IFGoperc.L), right olfactory cortex (OLF.R), bilateral gyrus rectus (REC), right supplementary motor area (SMA.R), and bilateral paracentral lobule (PCL; Figure 3, Table S6). Compared with the HC group, we localized a connected subnetwork involving more extensive brain regions with 21 nodes and 29 edges that were significantly decreased in the DPD group, which contained an extensive portion of the prefrontal (eg, the bilateral median cingulate and paracingulate gyri) and temporal-occipital (eg, the amygdala, bilateral FFG, and occipital lobe) lobes in addition to the same brain regions included in the different subnetwork between the NDPD and HC groups (Figure 3, Table S7). Most of these regions were the components of the prefrontal-limbic network and temporal-occipital visual cortex. In contrast, the DPD group did not show any alterations in functional connectivity compared with the NDPD group.

4 | DISCUSSION

In the present study, we comprehensively examined whole-brain resting-state networks for functional changes in DPD patients using graph theoretical and network-based analyses. Our findings revealed that the brain functional network of DPD patients preserved the small-world property, but the Eloc was significantly reduced compared with the HCs. In nodal metrics analyses, the degree of the occipital visual cortex in DPD group was found to be positively associated with the depressive symptoms. Meanwhile, there was a reorganization of the network’s hubs in the temporal visual cortex and PCG.L in the DPD group. Moreover, different functional connectivity trends were observed in the NDPD and DPD groups vs the HC group.

A small-world network involves a combination of a high $C_p$ (a measure of local network connectivity) and a short characteristic $L_p$ (a measure of global network connectivity), reflecting a highly effective topological organization combining regional specialization and efficient global information transfer to realize efficient transmission of information. Here, we found that the functional brain networks of the DPD, NDPD and HC individuals exhibited a small-world architecture, which is consistent with previous findings suggesting the preservation of a small-world architecture in the presence of pathology. Despite the common small-world topology, the Eloc showed significantly smaller values over a wide range of sparsity in

### Table 3 Hub regions in the HC, NDPD and DPD groups

| Groups | Region | Degree | Betweenness |
|--------|--------|--------|-------------|
| HC     | ITG.R | 17.195 | 61.361      |
|        | MTG.L | 16.853 | 48.454      |
|        | MTG.R | 16.564 | 44.172      |
|        | FFG.L | 16.630 | 45.940      |
|        | FFG.R | 16.826 | 54.120      |
| NDPD   | ITG.R | 17.195 | 61.361      |
|        | MTG.L | 16.853 | 48.454      |
|        | MTG.R | 16.564 | 44.172      |
|        | PCG.L | 16.039 | 46.224      |
| DPD    | NA    | NA     | NA          |

Note: The abbreviations of the 90 brain regions are given in Table 2. Abbreviations: DPD, Parkinson’s disease patients with depression; HC, healthy control; L, left hemisphere; NA, not applicable; NDPD, Parkinson’s disease patients without depression; R, right hemisphere.
the DPD patients relative to the HC subjects. Given that the small-world model reflects an optimal balance between local specialization and global integration, these results indicate a disturbance of the normal balance in functional brain networks of DPD patients. This disturbance can be attributed to the altered nodal characteristics and decreased functional connections in DPD patients. However, this significant difference did not survive between DPD vs NDPD groups. At the same time, our findings are not consistent with previous research reporting that small-world properties in PD patients differed from those in HCs, such as decreased Cp or increased Lp. These may be related to the effects of dopaminergic drugs. Functional magnetic resonance studies have revealed that degeneration of nigrostriatal neurons in PD may be associated with large-scale network reorganization and that levodopa tended to normalize the disrupted network topology in PD patients. Although all PD subjects underwent rs-fMRI after discontinuing antiparkinsonian medication for more than 12 hours, the interference of drugs could not be completely excluded.

The nodal degree is the sum of all binary/weighted edges of one node, which measures the single nodal connectivity to the rest of the nodes in a network. Regarding the significantly positive correlation between depressive symptoms and the betweenness centrality of IOG.R, which is the striate cortex regions of the visual cortex, previous studies have reported conclusions consistent with our findings. Some rs-fMRI studies have shown that the value of regional homogeneity in the occipital lobe was decreased and that the synchrony of interhemispheric resting-state functional connectivity was impaired in the occipital lobe in DPD patients. In particular, a graph theory study showed that the node topological properties of the bilateral lingual and bilateral inferior occipital regions were significantly associated with Geriatric Depressive Scale (GDS) scores in DPD patients. Moreover, studies also found that patients with DPD exhibited hyperperfusion and accelerated brainwave activity in the occipital cortex. Kim et al discovered that perfusion in the occipital lobe was increased and regional cerebral blood flow (rCBF) in the occipital cluster was positively related to the GDS scores in DPD patients. A quantitative electroencephalogram study showed the higher amplitude in beta in occipital lobe areas in rapid eye moment relative to nonrapid eye moment 2 were significantly different in DPD and NDPD patients. Increased cerebral blood flow and brainwave activity in these areas may accelerate effective information transmission. The mechanism remains unclear but may be related to the reduced γ-aminobutyric acid (GABA) levels, while GABAergic neurons are mostly distributed in the occipital cortex of depressed patients. Prior research has suggested that occipital levels of GABA were significantly lower in recovered depressed patients than in healthy controls. Inverse correlations between the GABA levels and rCBF in the brain have also been suggested by the previous literature. Further study revealed that increased baseline activation in the occipital cortex predicted antidepressant response. Accordingly, we considered that changes of topological attributes in occipital visual regions may serve as useful targets for biomarkers in assessing the severity and progression of DPD.

Additionally, the extrastriate cortex regions of the visual cortex (bilateral MTG and ITG.R) were identified as network hubs in the HC and NDPD groups, but not in the DPD group, which were consistent with a recent MRI study reporting that the node topological properties of the temporal visual area were significantly associated with depressive symptoms in PD patients. Previous studies have shown that neurodegenerative diseases target brain regions that are especially highly correlated in healthy subjects. These regions are the network hubs, which play a crucial role in the network, as they interact with many brain regions. One study showed that depression was correlated with impaired color vision in PD patients through clinical observation.
and inferred that the visual system is crucial in the depressive pathology in PD patients.\cite{39} We speculate that PD depression might disrupt the visual functional network and reorganize the network’s hubs.

In NBS analysis, compared with HCs, the functional connections between the regions of the temporal-occipital visual cortex and the prefrontal-limbic network were significantly weakened in DPD patients, which did not appear in the comparison between NDPD patients and HCs. The most common cognitive feature of depression is a processing bias toward negatively affective stimuli, which is associated with brain activation in visual areas involved in early visual processing of affective stimuli, limbic and paralimbic regions involved in evaluating and integrating sensory and affective information, and prefrontal areas involved in top-down emotion regulation.\cite{40} Combining our findings and those of previous studies, we propose that visual cortex dysfunction may play an important role in the pathophysiology of DPD and impact the connections with the brain regions involved in cognition and emotion, ultimately causing individuals to selectively attend to negative information and experience difficulty disengaging attention from negative stimuli. These attention biases subsequently reinforce a sad mood and contribute to a persistent depressive episode. Although no results showed significance between the DPD and NDPD groups under NBS correction, the different trends observed provided evidence that advances our understanding of the pathophysiological mechanism of DPD.

In addition, the PCG was one of the network hubs in the NDPD group, but not in the DPD group. The cingulate gyrus is an important area where the frontal cortex, insula, amygdala, and hypothalamus interconnect. As a part of the limbic system, it participates in emotion regulation, cognitive function and self-control. Posterior cingulate cortex (PCC) represents a core hub for the posterior subnetwork of the default mode network and plays a key role in integrating self-relative information, retrieval of episodic memory, and autobiographical search, the impairment of which contributes to the characteristic symptom of self-focused rumination and plays a part in the pathogenesis of primary depression.\cite{41,42} Gao et al\cite{43} found that patients with first-episode treatment-naive depression showed increased network homogeneity in the PCC. One study in unmedicated major depressive disorder patients reported higher functional connectivities between the PCC and lateral orbitofrontal cortex and between the angular and middle frontal gyri.\cite{44} A previous study also observed that functional connectivity in the right PCC was increased in DPD patients and negatively correlated with depression scores.\cite{45} Given these findings, we speculate that DPD and primary depression may share a similar pathological change and that the PCC plays a key hub role in the pathogenesis of primary depression, as well as in DPD patients.

![Figure 3](https://wileyonlineibrary.com)
Some limitations of our study should be noted. First, most of the subjects had regularly taken antiparkinsonian drugs, and the interference of drugs on the results was not completely eliminated. Second, this study had a cross-sectional design and a relatively small sample size. Third, although the AAL atlas is still widely applied to investigate human brain organizations, a previous study suggested that the topological organization of brain networks was affected by various parcellation strategies. Furthermore, this study adopted a single imaging technology to only preliminarily explore the possible relationship between changes in the brain functional network and DPD. Therefore, longitudinal follow-up observations are needed, drug-naive PD patients should be recruited, and different parcellation schemes should be used in conjunction in future large-scale studies using multimodal MRI techniques to further explore the pathogenesis of DPD.

In conclusion, our study explored the functional brain network in DPD patients based on rs-fMRI. Our results revealed that PD depression is associated with disruptions in the topological organization of functional brain networks, mainly involved the temporo-occipital visual cortex and the posterior cingulate gyrus. These findings may advance our current understanding of pathophysiological mechanism underlying DPD.

ACKNOWLEDGMENTS
This work was supported by the funding from the National Key R&D Program of China (No. 2017YFC1310200), National Natural Science Foundation of China (Nos. 81501112, 81471654, and 81974195), Guangdong Natural Science Foundation (No. 2016A030310327), Key Program of Natural Science Foundation of Guangdong Province, China (No. 2017B030311015), Guangzhou Municipal People’s Livelihood Science and Technology Project (No. 201803010085) and Medical Scientific Research Foundation of Guangdong Province, China (Nos. A2019437 and A2018137).

CONFLICT OF INTEREST
The authors have no conflict of interest to disclose.

DATA AVAILABILITY STATEMENT
The data that support the findings of this study are available in the supplementary material of this article.

ORCID
Li-Juan Wang https://orcid.org/0000-0003-1727-2670

REFERENCES
1. van der Hoek TC, Bus BA, Matui P, van der Mark MA, Esselink RA, Tendolkar I. Prevalence of depression in Parkinson’s disease: effects of disease stage, motor subtype and gender. J Neurol Sci. 2011;30(1-2):220-224.
2. Berg D, Postuma RB, Adler CH, et al. MDS research criteria for prodromal Parkinson’s disease. Mov Disord. 2015;30(12):1600-1611.
3. Shen CC, Tsai SJ, Peng CL, Kuo BI, Yang AC. Risk of Parkinson disease after depression: a nationwide population-based study. Neurology. 2013;81(17):1538-1544.
4. Jones JD, Marsiske M, Okun MS, Bowers D. Latent growth-curve analysis reveals that worsening Parkinson’s disease quality of life is driven by depression. Neuropsychology. 2015;29(4):603-609.
5. Bullmore E, Sporns O. Complex brain networks: graph theoretical analysis of structural and functional systems. Nat Rev Neurosci. 2009;10(3):186-198.
6. Huang LC, Wu PA, Lin SZ, Pang CY, Chen SY. Graph theory and network topological metrics may be the potential biomarker in Parkinson’s disease. J Clin Neurosci. 2019;68:235-242.
7. Hu X, Qian L, Zhang Y, et al. Topological changes in white matter connectivity network in patients with Parkinson’s disease and depression. Brain Imaging Behav. 2020. https://doi.org/10.1007/s11682-019-00208-2 [Epub ahead of print].
8. Gou L, Zhang W, Li C, et al. Structural brain network alteration and its correlation with structural impairments in patients with depression in de novo and drug-naive Parkinson’s disease. Front Neurol. 2018;9:608.
9. Bai F, Shu N, Yuan Y, et al. Topologically convergent and divergent structural connectivity patterns between patients with remitted geriatric depression and amnestic mild cognitive impairment. J Neurosci. 2012;32(12):4307-4318.
10. Korgaonkar MS, Fornito A, Williams LM, Grieve SM. Abnormal structural networks characterize major depressive disorder: a connectome analysis. Biol Psychiatry. 2014;76(7):567-574.
11. Tinaz S, Lauro PM, Ghosh P, Lungu C, Horovitz SG. Changes in functional organization and white matter integrity in the connectome in Parkinson’s disease. NeuroImage Clin. 2017;13:395-404.
12. Starkstein S, Dragovic M, Jorgie R, et al. Diagnostic criteria for depression in Parkinson’s disease: a study of symptom patterns using latent class analysis. Mov Disord. 2011;26(12):2239-2245.
13. Uher R, Payne JL, Pavlova B, Perlis RH. Major depressive disorder in DSM-5: implications for clinical practice and research of changes from DSM-IV. Depress Anxiety. 2014;31(6):459-471.
14. Jenkinson M, Bannister P, Brady M, Smith S. Improved optimization for the robust and accurate linear registration and motion correction of brain images. NeuroImage. 2002;17(2):825-841.
15. Yan CG, Craddock RC, Zuo XN, Zang YF, Milham MP. Standardizing the intrinsic brain: towards robust measurement of inter-individual variation in 1000 functional connectomes. NeuroImage. 2013;80:246-262.
16. Yan CG, Wang XD, Zuo XN, Zang YF. DPABI: data processing & analysis for (resting-state) brain imaging. Neuroinformatics. 2016;14(3):339-351.
17. Wang J, Wang X, Xia M, Liao X, Evans A, He Y. GRETA: a graph theoretical network analysis toolbox for imaging connectomics. Front Hum Neurosci. 2015;9:386.
18. Tzourio-Mazoyer N, Landeau B, Papathanassiou D, et al. Automated anatomical labeling of activations in SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain. NeuroImage. 2002;15(1):273-289.
19. Chen L, Fan X, Li H, et al. Topological reorganization of the default mode network in severe male obstructive sleep apnea. Front Neurol. 2018;9:363.
20. Salzwedel AP, Gao W, Andres A, et al. Maternal adiposity influences neonatal brain functional connectivity. Front Hum Neurosci. 2018;12:514.
21. He Y, Dagher A, Chen Z, et al. Impaired small-world efficiency in structural cortical networks in multiple sclerosis associated with white matter lesion load. Brain. 2009;132(12):3366-3379.
22. Zalesky A, Fornito A, Bullmore ET. Network-based statistic: identifying differences in brain networks. NeuroImage. 2010;53(4):1197-1207.
23. Pereira JB, Aarsland D, Ginestet CE, et al. Aberrant cerebral network topology and mild cognitive impairment in early Parkinson’s disease. Hum Brain Mapp. 2015;36(8):2980-2995.
24. Armstrong CC, Moody TD, Feusner JD, et al. Graph-theoretical analysis of resting-state fMRI in pediatric obsessive-compulsive disorder. *J Affect Disord*. 2016;193:175-184.

25. Latora V, Marchiori M. Efficient behavior of small-world networks. *Phys Rev Lett*. 2001;87(19):198701.

26. Liao X, Vasilakos AV, He Y. Small-world human brain networks: Perspectives and challenges. *Neurosci Biobehav Rev*. 2017;77:286-300.

27. Suo X, Lei D, Li N, et al. Functional brain connectome and its relation to Hoehn and Yahr stage in Parkinson disease. *Radiology*. 2017;285(3):904-913.

28. Gottlich M, Munte TF, Heldmann M, Kasten M, Kramer UM. Altered resting state brain networks in Parkinson’s disease. *PLoS One*. 2013;8(10):e77336.

29. Berman BD, Smucny J, Wylie KP, et al. Levodopa modulates small-world architecture of functional brain networks in Parkinson’s disease. *Mov Disord*. 2016;31(11):1676-1684.

30. Sheng K, Fang W, Su M, et al. Altered spontaneous brain activity in patients with Parkinson’s disease accompanied by depressive symptoms, as revealed by regional homogeneity and functional connectivity in the prefrontal-limbic system. *PLoS One*. 2014;9(1):e84705.

31. Zhu Y, Song X, Xu M, et al. Impaired interhemispheric synchrony in Parkinson’s disease with depression. *Sci Rep*. 2016;6:27477.

32. Kim YD, Jeong HS, Song IU, Chung YA, Namgung E, Kim YD. Brain perfusion alterations in depressed patients with Parkinson’s disease. *Ann Nucl Med*. 2016;30(10):731-737.

33. Liu K, Ma Q, Wang M. Comparison of quantitative electroencephalogram during sleep in depressed and non-depressed patients with Parkinson’s disease. *Med Sci Monit*. 2019;25:1046-1052.

34. Bhagwagar Z, Wylezinska M, Jezzard P, et al. Reduction in occipital cortex gamma-aminobutyric acid concentrations in medication-free recovered unipolar depressed and bipolar subjects. *Biol Psychiatry*. 2007;61(6):806-812.

35. Roland PE, Friberg L. The effect of the GABA-A agonist THIP on regional cortical blood flow in humans. A new test of hemispheric dominance. *J Cereb Blood Flow Metab*. 1988;8(3):314-323.

36. Spanaki MV, Siegel H, Kopylev L, et al. The effect of vigabatrin (gamma-vinyl GABA) on cerebral blood flow and metabolism. *Neurology*. 1999;53(7):1518-1522.

37. Furey ML, Drevets WC, Hoffman EM, Frankel E, Speer AM, Zarate CA Jr. Potential of pretreatment neural activity in the visual cortex during emotional processing to predict treatment response to scopolamine in major depressive disorder. *JAMA Psychiatry*. 2013;70(3):280-290.

38. van den Heuvel MP, Sporns O. Network hubs in the human brain. *Trends Cogn Sci*. 2013;17(12):683-696.

39. Li DK, Liu FT, Chen K, et al. Depressive symptoms are associated with color vision but not olfactory function in patients with Parkinson’s disease. *J Neuropsychiatry Clin Neurosci*. 2018;30(2):122-129.

40. Ho TC, Zhang S, Sacchet MD, et al. Fusiform gyrus dysfunction is associated with perceptual processing efficiency to emotional faces in adolescent depression: a model-based approach. *Front Psychol*. 2016;7:40.

41. Whitfield-Gabrieli S, Ford JM. Default mode network activity and connectivity in psychopathology. *Annu Rev Clin Psychol*. 2012;8:49-76.

42. Buckner RL, Andrews-Hanna JR, Schacter DL. The brain’s default network: anatomy, function, and relevance to disease. *Ann N Y Acad Sci*. 2008;1124:1-38.

43. Gao Y, Wang M, Yu R, et al. Abnormal default mode network homogeneity in treatment-naive patients with first-episode depression. *Front Psychiatry*. 2018;9:697.

44. Rolls ET, Cheng W, Du J, et al. Functional connectivity of the right inferior frontal gyrus and orbitofrontal cortex in depression. *Soc Cogn Affect Neurosci*. 2020;15:75-86.

45. Lou Y, Huang P, Li D, et al. Altered brain network centrality in depressed Parkinson’s disease patients. *Mov Disord*. 2015;30(13):1777-1784.

46. Wang J, Wang L, Zang Y, et al. Parcellation-dependent small-world brain functional networks: a resting-state fMRI study. *Hum Brain Mapp*. 2009;30(5):1511-1523.

**SUPPORTING INFORMATION**

Additional supporting information may be found online in the Supporting Information section.

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**How to cite this article:** Qiu Y-H, Huang Z-H, Gao Y-Y, et al. Alterations in intrinsic functional networks in Parkinson’s disease patients with depression: A resting-state functional magnetic resonance imaging study. *CNS Neurosci Ther*. 2021;27:289–298. [https://doi.org/10.1111/cns.13467](https://doi.org/10.1111/cns.13467)