Technical Note

Preliminary Report of Three-Dimensional Reconstructive Intraoperative C-Arm in Percutaneous Vertebroplasty

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Objective: Percutaneous vertebroplasty (PVP) is usually carried out under three-dimensional (2D) fluoroscopic guidance. However, operative complications or bone cement distribution might be difficult to assess on the basis of only 2D radiographic projection images. We evaluated the feasibility of performing an intraoperative and postoperative examination in patients undergoing PVP by using three-dimensional (3D) reconstructive C-arm.

Methods: Standard PVP procedures were performed on 14 consecutive patients by using a Siremobil Iso-C3D and a multidetector computed tomography machine. Post-processing of acquired volumetric datasets included multiplanar reconstruction (MPR) and surface shaded display (SSD). We analyzed intraoperative and immediate postoperative evaluation of the needle trajectory and bone cement distribution.

Results: The male : female ratio was 2 : 12; mean age of patients, 70 (range, 77-54) years; and mean T score, -3.4. The mean operation time was 52.14 min, but the time required to perform and post-process the rotational acquisitions was 7.76 min. The detection of bone cement distribution and leakage after PVP by using MPR and SSD was possible in all patients. However, detection of the safe trajectory for needle insertion was not possible.

Conclusion: 3D rotational image acquisition can enable intra- or post-procedural assessment of vertebroplasty procedures for the detection of bone cement distribution and leakage. However, it is difficult to assess the safe trajectory for needle insertion.

Key Words: Vertebroplasty · Intraoperative 3D imaging · Complication · Feasibility.

INTRODUCTION

Percutaneous vertebroplasty (PVP) was developed by Galibert and Deramond in 1987, and it involves the injection of bone cement (polymethylmethacrylate; PMMA) into a collapsed vertebral body. The main indications have been extended to the treatment of painful osteoporotic compression fractures, vertebral myeloma, and metastases.

In many centers, all phases of the PVP procedure are usually performed under two-dimensional (2D) fluoroscopic guidance. However, the operative complications, e.g., cement extravasation into critical structures such as veins at the vertebral foramen, or bone cement distribution might be difficult to assess on the basis of only 2D radiographic projection images.

Computed tomography (CT) in combination with fluoroscopy-guided PVP was first described by Gangi et al. in a series of 10 patients. CT in combination with fluoroscopy during vertebroplasty provides excellent imaging and enables exact positioning of the vertebroplasty needle. Further, this technique facilitates optimal filling of the vertebral body because of detailed localization of the injected bone cement. Furthermore, potential bone cement leakages can be detected, especially cement leakage into smaller veins. However, CT in combination with fluoroscopy-guided PVP has some shortcomings: this technique requires expensive equipment and a large space, and it is difficult to maintain aseptic conditions during the procedure.

In vascular intervention, rotational image acquisition with a C-arm fluoroscopy unit is an established method. With the introduction of rotational image acquisition, it became possible to acquire high-resolution three-dimensional (3D) angiographic images. However, in vertebroplasty, this technique is not used. We evaluated the feasibility of performing standard PVP procedures by using 3D rotational acquisitions by Siremobil Iso-C3D (Siemens Medical Solutions, Erlangen, Germany).
**MATERIALS AND METHODS**

**Patients and PVP procedure**

Fourteen consecutive patients (women, 12; men, 2; mean age, 70 years; age range, 54-77 years) in whom transpedicular PVP procedures were performed using a Siremobil Iso-C$^{10}$ for intraoperative procedural control were studied. The indications for PVP were metastasis (n=1) and osteoporotic compression fractures (n=13). The total number of vertebrae controlled with 3D acquisitions and CT was 15 (thoracic, 5; lumbar, 9; sacral, 1) (Table 1). In all patients, we initially performed vertebroplasty by unilateral transpedicular approach and total twice single rotational acquisition was performed at after needle and PMMA insertion. If the injected cement was not evenly distributed, we performed transpedicular approach at contralateral side. This acquisition was focused on the region where visualization of needle trajectory, bone cement distribution, and leakage was of the most interest.

**Image acquisition, post-processing, and analysis**

3D rotational images were acquired immediately after needle insertion and PMMA injection, with the patient remaining in the prone position (lumbar and thoracic spine) on the table. Patients who were awake were asked to hold their breath during image acquisition. Images were acquired using a Siremobil Iso-C$^{10}$ (Siemens Medical Solutions, Erlangen, Germany) that allows creation of 3D anatomical images, with the anatomy to be imaged positioned in the system isocenter. The rotational scan covers 190 degrees of the circular trajectory and is accomplished in 30 seconds with 50 images per scan. The field of view could be chosen from 17 to 38 with a matrix of 1024×1024. To obtain images optimized for bone display, a dedicated acquisition system program (“bone run”) was selected. The images from rotational acquisition were transferred to the commercially available post-processing station through a conventional network connection. To transfer 254 images, 5-6 seconds were required. The reconstructed data set was visualized using different display techniques such as multiplanar reformat and shaded surface display. With these display techniques, it was possible either to display a 3D model of the entire volume or to analyze image slabs in 3 perpendicular views with the ability to cross-reference the images (Fig. 1).

**Evaluated parameters**

Two independent observers, blinded to any other information relating to the subjects, measured the distribution and leakage of cement and safety of needle trajectory (Fig. 2). We grouped the cement distribution (regional, focal distribution of cement; unilateral, unilateral distribution of cement; bilateral - uneven, bilateral lateral distribution of cement but separated mass; bilateral-even, bilateral single mass of cement) and the presence of cement leakage (posterior to the vertebra, paravertebral; anterior or lateral to the vertebral body, foraminal, and in the region of the vessels).

**RESULTS**

On average, 1.07 vertebrae were treated per patient. In all cases, the time from rotational image acquisition to visualization of 3D volume images was less than 10 minutes. There was 1 vertebra in the regional group, 3 vertebrae in the bilateral - uneven group, and 11 vertebrae in the bilateral-even group. The 6 cases of regional or unilateral distribution of bone cement during operation received additional bone cement injection, but in 3 of 6 cases, a continuous-bivertebrate distribution could not be achieved. On reconstructive images, leakage was found in 6 (40%) of 15 vertebrae, with localization in the paravertebral muscular area [4 (26.7%) vertebrae] and vascular leakage [2 (13.3%) vertebrae].

**Table 1. Summary of case**

| Case | Age | Sex | Level | BMD | Amount of cement | Cement distribution | 3D acquisition time (min) | Direction of leakage | Safety of needle trajectory |
|------|-----|-----|-------|-----|-----------------|---------------------|-------------------------|----------------------|--------------------------|
| 1    | 77  | M   | L2    | -2.8| 4               | Bilateral-even      | 7                       | Paravertebral mm      | None diagnostic          |
| 2    | 76  | F   | L2    | -2.9| 4               | Bilateral-even      | 8                       | No                    | None diagnostic          |
| 3    | 76  | F   | L1    | -2.5| 4.4             | Bilateral-even      | 8                       | Paravertebral vein     | Non diagnostic           |
| 4    | 66  | F   | T12   | -3   | 3               | Bilateral-even      | 7                       | Paravertebral vein     | None diagnostic           |
| 5    | 60  | F   | S1    | -2.9| 3               | Regional            | 9                       | No                    | None diagnostic          |
| 6    | 59  | M   | L1    | -3.5| 4.5             | Bilateral-even      | 8                       | No                    | None diagnostic          |
| 7    | 54  | F   | L1    | -3.7| 1.5             | Bilateral-even      | 9                       | Paravertebral mm       | None diagnostic          |
| 8    | 75  | F   | T12   | -3.9| 5               | Bilateral-even      | 8                       | Paravertebral mm       | None diagnostic          |
| 9    | 77  | F   | T7    | -3.6| 4               | Bilateral-even      | 7                       | Paravertebral mm       | None diagnostic          |
| 10   | 79  | F   | L1    | -5   | 4.4             | Bilateral - uneven  | 6                       | No                    | None diagnostic          |
| 11   | 74  | F   | L3    | -3.4| ?               | Bilateral - uneven  | 9                       | No                    | None diagnostic          |
| 12   | 73  | F   | T12   | -3.5| 3               | Bilateral-even      | 8                       | No                    | None diagnostic          |
| 13   | 68  | F   | L4    | -3.5| 6               | Bilateral - uneven  | 7                       | No                    | None diagnostic          |
| 14   | 69  | F   | L5    | -3.4| 3               | Bilateral-even      | 7                       | No                    | None diagnostic          |

3D: three-dimensional
and is usually asymptomatic. The visualization provided by 2D fluoroscopy images is sufficient to control clinically significant cement leakages occurring after the PVP procedure. However, it can be difficult to exactly localize cement leakage on only 2D fluoroscopic images. If cement leakage to critical anatomic structures such as the neural foramen or posterior epidural space is suspected, it is important to have exact imaging information for performing further workup and administering appropriate treatment to the patient. Furthermore, immediate availability of the 3D image data set after the cement injection (while the patient is still on the operating table) by using the same X-ray equipment facilitates 1) earlier and exact detection of a complication, 2) the therapeutic decision process, and 3) initiation of protective procedures. In our study, we could early and exact detect the leakage and uneven distribution of the bone cement and perform the rapid therapeutic and protective procedure for bone cement associated complication. However, the rate of bone cement leakage of this study was 40%, which was not significantly higher than that in previously reported data (range, 8-87.5%). Therefore, this 3D image CT guidance vertebroplasty technique seems to be of relatively helpful to detection and protection of bone cement associated complication.

Technical complications are rare and have been reported in less than 1% of the treated patients. One of the major technical complications is a neural injury due to violation of the pedicle wall by the needle. Obtaining volumetric images immediately after an intervention is the key advantage of rotational acquisitions as compared with CT imaging. However, the resolution of the rotational images was clearly inferior as compared to that of CT images. Because of the lower resolution on rotational images, the safe trajectory for needle insertion could not be detected in all of our cases. Eventually, 3D image CT guidance vertebroplasty technique would be helpful in complicated patients who need to exact insertion of the bone cement such as vertebra plana or need to be operated under the general anesthesia.

CONCLUSION

Our preliminary experiences indicate that 3D rotational image acquisition can be of relatively helpful to intra- or post-procedural assessment of the vertebroplasty procedure and detection...
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