Bioglass: A novel biocompatible innovation

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Abstract

Advancement of materials technology has been immense, especially in the past 30 years. Ceramics has not been new to dentistry. Porcelain crowns, silica fillers in composite resins, and glass ionomer cements have already been proved to be successful. Materials used in the replacement of tissues have come a long way from being inert, to compatible, and now regenerative. When hydroxyapatite was believed to be the best biocompatible replacement material, Larry Hench developed a material using silica (glass) as the host material, incorporated with calcium and phosphorous to fuse broken bones. This material mimics bone material and stimulates the regrowth of new bone material. Thus, due to its biocompatibility and osteogenic capacity it came to be known as “bioactive glass-bioglass.” It is now encompassed, along with synthetic hydroxyapatite, in the field of biomaterials science known as “bioactive ceramics.” The aim of this article is to give a bird’s-eye view, of the various uses in dentistry, of this novel, miracle material which can bond, induce osteogenesis, and also regenerate bone.

Key words: Biocompatible, bioinert, bioregenerative, hydroxyapatite, osteogenic

INTRODUCTION

A glimpse through the history of development of materials used in dentistry, specifically replacement materials, shows that the aim has been to create materials that were as chemically inert as possible. In mid 60s, the biocompatibility and long-term survival of the material was achieved by minimizing the material-host interaction. As the materials used at that time were mostly metallic, this led to corrosion and eventual failure caused by the aggressive nature of body fluids. This led to the search of materials that could withstand the chemical attack of the body.

In the late 1960s and early 1970s, the search for better biocompatibility of implant materials resulted in the new concept of bioceramic materials that would mimic natural bone tissue. Hydroxyapatite, a naturally occurring ceramic mineral, was also the mineral component of bone. Thus, only synthetic hydroxyapatite was believed to be entirely compatible with the body.

During this period, Professor Hench came up with a new biocompatible material using silica (glass) as a base material that could be mixed with other ingredients such as calcium to unite fractured bones. This mimics normal bone and stimulates the regrowth of new bone between the fractures.[1,2] By using this material, the trend of implant materials was shifted to stimulate body’s own regenerative capabilities. This new glass material on dissolving, in normal physiological environment, activates genes controlling osteogenesis and growth factor production[2-4] (within 48 hours) with bone produced of equivalent quality to natural bone.[3,5] The trabecular bone growth and quantity were much more than produced by synthetic hydroxyapatite.[6,7] After implantation of this material in bone tissue, these glass materials resisted removal from the implant site – which was coined as “bonded to bone” by Hench.[8,9] Hench used the term “bioactive glass” to describe this attachment.[1,10,11] A bioactive material is defined as a material that elicits a specific biological response at the interface of the material, which results in the formation of a bond between the tissue and that material.[12,13] The term bioactive was later applied to encompass the entire field of biomaterials science known as bioactive ceramics.[14]

The gene activation, bone regenerative capability with
better quality and quantity of bone equivalent to normal bone, and high level of bioactivity are unique only to bioglass when compared with synthetic hydroxyapatite and any other allograft, which more than justifies the use of bioglass.

The other advantages of bioglass over synthetic hydroxyapatite are the biological fixation, and the capability of bonding to both hard and soft tissues, whereas hydroxyapatite binds only to hard tissues and also needs an exogenous covering to hold the implants in place.

**Composition and Mechanism of Activity**

The original bioglass (45S5) composition is as follows: 45% silica (SiO$_2$), 24.5% calcium oxide (CaO), 24.5% sodium oxide (Na$_2$O), and 6% phosphorous pentoxide (P$_2$O$_5$) in weight percentage. Bioglass material is composed of minerals that occur naturally in the body (SiO$_2$, Ca, Na$_2$O, F, H, and P), and the molecular proportions of the calcium and phosphorous oxides are similar to those in the bones. The surface of a bioglass implant, when subjected to an aqueous solution, or body fluids, converts to a silica-CaO/P$_2$O$_5$-rich gel layer that subsequently mineralizes into hydroxycarbonate in a matter of hours. More the dissolution, better the bone tissue growth. This gel layer resembles hydroxyapatite matrix so much that osteoblasts were differentiated and new bone was deposited.

Ca$_5$(PO$_4$)$_3$(OH) is the chemical formula for hydroxyapatite, a natural mineral form of calcium apatite and usually written as Ca$_{10}$(PO$_4$)$_6$(OH)$_$_2.

The bioactivity level of any material is measured by bioactivity Index ($I_B$). Bioactivity Index of a material is the time taken for more than half of the interface to bond, i.e.,

$$I_B = 100/t_{0.5bb}$$

Any material with the value of $I_B$ greater than 8, like 45S5, will bond to both soft and hard tissues. Materials such as synthetic hydroxyapatite with $I_B$ value < 8 but > 0 will bind only to hard tissue. The typical composition of the bioglass and bioceramics is indicated in Table 1.

When the proportions of these minerals are altered, the properties of the bioglass change, which can be suited to be used in various body parts accordingly.

As depicted in the triangle [Figure 1], varying proportions of the components cause the bioglass to be bioinert, bioresorbable, or bioregenerative.

Bioglass is available in multiple forms: Particulate, pellets, powder, mesh, and cones. Interestingly it can be moulded into any desired form [Figure 2].

**BIOGLASS AS GRAFT MATERIAL**

Materials chosen for grafting need to be biocompatible, bioresorbable, and osteogenic. Treatment for the elimination of osseous defects due to periodontal diseases, pathologies, and surgeries include autogenous bone grafts, alloplast, guided tissue regeneration, combination of guided tissue regeneration and decalcified freeze dried bone.

Limitations of autogenous bone grafts are additional surgical trauma and not enough tissue material to fill the defect. To overcome these restrictions, alloplastic materials were used. But again adverse immune response and disease transmission have restricted its widespread acceptance. The membrane exposure and the local infection that follows in guided tissue regeneration obstruct bone formation.

The last three decades saw the trials of many glass and glass-ceramic compositions. The glass-silicate composition developed by Hench showed bonding to bone. The bioactive glass has been observed to bond with certain connective tissue through collagen formation with the glass surface. Bioactive glass with its interconnected porosity has added advantages in hard-tissue prosthesis. The porous structure
Bioglass was used in particle form to fill periodontal osseous defects. Bone was seen to be surrounding individual particles from many sites. Twenty patients age 23–55 years (44 sites) with intrabony defects completed the 1-year study. Follow-up was carried out weekly, at 3 months, 6 months, 9 months, and 1 year post surgery. Results showed a significant increase in radiographic density and volume between the defects treated with bioactive glass when compared with those treated with surgical debridement only. Thus, bioactive glass was found to be effective in the treatment of intrabony defects.\textsuperscript{[27]}

Another study\textsuperscript{[28]} was conducted with bioglass particulates in periodontal osseous defects of 12 patients. Data was collected initially and at 3, 6, 24 months post-treatment intervals. Considerable improvements of all clinical parameters of mean probing depth reduction, mean attachment gain, and mean radiographic bone fill were noted. Follow-up of over 24 months showed stable results. The material elicited extraordinary tissue response and hassle-free handling.

**BIOGLASS AS ENDOSSEOUS IMPLANT**

After dental extraction, resorption of alveolar bone affects majority of patients.\textsuperscript{[29-31]} This resorption leads to ill-fitting dentures resulting in compromised masticatory efficiency, oral and systemic health problems, and esthetics. Alveolar bone height is maintained on stimulation by the periodontal membrane and teeth or roots being present.\textsuperscript{[32,33]} After extraction, stimulation is lost to the alveolar bone and the pressure from dentures cause bone resorption.\textsuperscript{[34,35]} The resorption rate varies with from individual to individual and at varying levels in the same individual.\textsuperscript{[32,33,36]}

Many treatment modalities have been suggested for

### Table 1: Composition of bioglass and glass ceramics

| Glass     | SiO\textsubscript{2} | P\textsubscript{2}O\textsubscript{5} | CaO | Ca(PO\textsubscript{3})\textsubscript{2} | CaF\textsubscript{2} | Na\textsubscript{2}O | Others | Properties |
|-----------|---------------------|-----------------|-----|-----------------|-----------------|-----------------|--------|------------|
| Bioglass 425.1 | 40.1 | 2.6 | 29.0 | 26.3 | Mol% |
| Bioglass 465.2 | 46.1 | 2.6 | 26.9 | 24.4 | Mol%; best tissue bonding of bioglass formulas |
| Bioglass 495.4 | 49.1 | 2.6 | 25.3 | 23.8 | Mol% |
| Bioglass 525.6 | 52.1 | 2.6 | 23.8 | 21.5 | Mol% |
| Bioglass 555.3 | 55.1 | 2.6 | 22.2 | 20.1 | Mol% |
| Bioglass 605.3 | 60.1 | 2.6 | 19.6 | 17.7 | Mol%, no phosphate film formed |
| Bioglass 455S | 45 | 6 | 24.5 | 24.5 | The original Bioglass formulation; binds with bone and soft tissues |
| Bioglass 455SF | 45 | 6 | 12.25 | 12.25 | 24.5 |
| Bioglass 455S.4F | 45 | 6 | 14.7 | 9.8 | 24.5 |
| Bioglass 405SB5 | 40 | 6 | 24.5 | 24.5 | 5 B\textsubscript{2}O\textsubscript{3} |
| Bioglass 525.6 | 52 | 6 | 21 | 21 |
| Bioglass 555.4 | 55 | 6 | 19.5 | 19.5 |
| Bioglass 8625 | ? | ? | ? | ? | \textsubscript{Fe}_3 \textsubscript{O}_5 | Highly biocompatible, does not bind with tissues, fibrous encapsulation; absorbs infrared radiation, can be laser sealed, used for RFID tag encapsulation |
augmentation of the atrophic ridge. Although autogenous bone grafting can be a recommended treatment modality and also with reduced antigenicity of freeze dried bone rejection, infections and transmission of disease limit its usage.

Ankylosis, resorption, and pocket formation make replantation of natural roots a failure. Thus, maintaining the residual alveolar ridge is better than trying to augment it. While many materials such as carbon, calcium phosphate ceramics, tricalcium phosphate, hydroxyapatite, coraline hydroxyapatite, and bioglass have been used in augmentation of alveolar ridge, dehiscence of these materials, mostly within 12 months, made implantation difficult.

Considering these obstacles, bioglass was the most promising implant material, as proved by the study carried out by Stanley et al., using cone-shaped bioglass. The study was done on baboons for 2 years. Bioglass implants were placed in the extracted sockets of incisors, splinted to adjacent natural teeth for 3 months and then desplinted. Dehiscence was not encountered even at 12 months, compared with dehiscence at 10 months with other materials. Infectionless normal tissue healing with new bone formation as sighted in radiographs made bioglass a highly biocompatible innovation.

**BIOGLASS AS REMINERALIZING AGENT**

Around 35% of patients complain of dentinal hypersensitivity. Initial treatment was by calcium phosphate precipitation method using dentin etching. The characteristic osteogenic activity of bioactive and biocompatible glass made it worth its trial in occluding dentinal tubules. A new dentifrice formulation containing a modified bioglass material, replacing a part of the abrasive silica component, was compared with original 45S6 bioactive glass. The results evidenced that original bioglass dislodged easily when compared with modified bioglass, proving that bioglass, when used with a suitable vehicle, can be an excellent treatment for dentine sensitivity.

A second study compared mineralization of bioactive glass S53P4 with regular commercial glass. The bioactive glass released more silica than commercial glass along with lesser decalcification during the process when pretreated with bioactive glass. Thus, bioactive glass S53P4 is more efficient in treatment of dentinal hypersensitivity.

In support to the above study, Salonen et al. proved that S53P4 induced tissue mineralization at the glass-tissue interface and elsewhere. The study widened the use of bioglass in treatment of caries prophylaxis, in dentinal hypersensitivity, as root apex sealer, and as metal implant coating.

Among the uses of bioactive glass, the efficacy of sol-gel bioglass particles, and melt-driven bioglass particles were tested and compared. Dentine treated with melt-driven bioglass showed an apatite layer, which was continuous, adherent, and with particle formation. Bioerodible gel films have also been proved to be useful in the delivery of remineralizing agents.

**BIOGLASS AS ANTIBACTERIAL AGENT**

The reactions of bioglass in aqueous environment, leading to osseointegration prompted scientists to check its antibacterial activity. Streptococcus sanguis, Streptococcus mutans, and Actinomyces viscosus were suspended in nutrient broth and artificial saliva or Dulbecco’s modified Eagle’s medium plus 10% fetal calf serum with or without particulate bioglass. There was considerable reduction in the viability of all bacteria tested, in both media, when compared with inert glass controls. In conclusion, the antibacterial effect of bioglass was attributed to its alkaline nature.

**BIOGLASS IN DRUG DELIVERY**

The basic criteria for selection of any drug delivery system should be that it is inert; biologically compatible; has good mechanical strength; is good from the aspect of patient comfort; has the ability to carry high doses of the drug, with no risk of accidental release; and is in easy administering, removal, fabrication, and sterilization. There are three basic mechanisms through which active agents can be delivered: By diffusion, activation of solvent or swelling, and degradation.

Controlled drug delivery means preplanned delivery of a drug. The aim was to be more effective without possibilities of increased or decreased dosages, and also greater patient acceptance, maximal usage of the drug, with least administrations.

The importance is more so even when this accuracy is limited while using conventional drugs or injections. For example, when water soluble drugs should be slowly released, low soluble drugs should be released fast, specific-site delivery, nanoparticulate drug delivery systems, and where carriers...
should be quickly removed. Studies have proved that bioglass in such cases can be a successful carrier in drug delivery.

A study used Fick’s diffusion law to treat osteomyelitis with teicoplanin.[50] Teicoplanin was the liquid and borate bioactive glass the solid carrier along with chitosan, citric acid, and glucose. The results of the study showed bioactivity of hydroxyapatite forming from the bioglass when the drug was being released. This system cured the osteomyelitis in tibial bone of rabbits in vivo, and also promoted formation of the tibial bone.

Bioglass has been tried as a vehicle for drug delivery. Vancomycin on bioglass carrier has been tested for treating osteomyelitis with success.[51]

Indomethacin was tried with self-setting bioactive cement based on CaO-SiO$_2$-P$_2$O$_5$ glass. This mixture hardened and formed hydroxyapatite in about 5 minutes with volume shrinkage of 5% in simulated body fluid.[52]

The fast-acting anti-inflammatory drug ibuprofen was released in the first 8 hours when immersed in simulated body fluid.[53,54]

**BIOGLASS IN BONE TISSUE ENGINEERING**

One of the biggest hurdles in tissue engineering was to mimic the extracellular matrix. Scaffolds built using biocomposite nanofibers and nanohydroxyapatite were naturally very porous, which in turn facilitated good cell occupancy, vascularity, movement of nutrients, and metabolic waste products. Studies comparing bioinert with bioactive glass ceramic templates, produced increased osteoblast proliferation and differentiation. This system helped the human fetal osteoblasts to adhere, migrate, proliferate, and mineralize into bone, which was a tremendous step ahead in the bone defect filling.[3,55]

**CONCLUSION**

On critical analysis, Young’s modulus of bioglass being between 30 and 50 GPa, nearly that of natural bone, is a great advantage.[20] Maybe a small disadvantage is the low mechanical strength and decreased fracture resistance. This can be easily overcome by altering the composition, using it in low load-bearing areas, and using it for the bioactive stage. Very clearly, the disadvantages of bioglass are minimal compared with its versatile strength and huge foray of uses.

The replacement of tissues demands very high importance in this technological era. As highlighted in the present article, bioglass is a versatile replacement material, as it is available in multiple forms and also can be moulded into desired forms as per the need of the user. Thus, its scope for use also increases manifold. After two decades of being in use, the most telling is that bioglass has not reported any adverse responses when used in the body. As the use of these compositions increases, in varying clinical fields, it will bring into sight, better applications in repair as well as regeneration of natural tissues.

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