Polyaniline-CdS Quantum Dots Composite for Mediator Free Biosensing

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Abstract

A novel route has been introduced to fabricate the composite of polyaniline (PANI) and cadmium sulphide quantum dots (CdS-QD) using electrochemical polymerization technique for mediator free biosensing. The synthesis process involves in situ formation of CdS quantum dots that provide template for electro-polymerization of aniline resulting in nanostructured PANI-(CdS-QD) film deposition on the indium-tin-oxide (ITO) coated glass plate. Transmission electron microscopy and scanning electron microscopy have been used to reveal the formation of CdS-QD and morphological changes involved during incorporation of CdS in PANI matrix and while immobilization of cholesterol oxidase (ChOx). The UV–visible and FT-IR investigations show the formation of PANI-(CdS-QD) composite at the molecular level. This matrix has been utilized for the covalent immobilization of cholesterol oxidase to explore its application for cholesterol sensing. The results of the CV and EIS studies indicate enhanced electrochemical and charge transfer behaviour of the composite. The response studies, carried out using CV technique, reveal this ChOx/ PANI-(CdS-QD)/ITO bioelectrode to detect cholesterol in the concentration range of 50 to 500 mgdL−1 with good detection limit (47.8 mgdL−1) and low Kth value (0.82 mM).

Keywords: Polyaniline; Cadmium Sulphide; Quantum Dots; Conducting Polymers; Biosensor

Introduction

Conducting polymers are known to be compatible with biological molecules and also have the quality to efficiently transfer the electric charges produced during the biochemical reactions through their conjugated backbone. In the past few years many conducting polymers have been used with the different prospects for biosensing applications [1]. Among all these polymers, polyaniline is known to be semi-flexible and has been found to provide the efficient medium for electron transfer. The chemical and structural flexibility surrounding its amine nitrogen linkages for the immobilization of desired biomolecules has attracted much efforts towards the various applications in the field of biosensing due to its electrochemical, electronic, optical and electro-optical properties [2,3].

Synthesis and functionalization of nanomaterials have aroused much interest due to large surface-to-volume ratio and the quantum confinement effect in semiconductor nanomaterials in which appropriate surface modification by stabilizers can remove localized surface-trap states resulting in increased quantum yield of the excitonic emission. Besides this, quantum dots are known to have extraordinary surface-trap states resulting in increased quantum yield of the excitonic emission. Besides this, quantum dots are known to have extraordinary electron and optical properties due to their size-tunability, surface-capping chemistry, high quantum yield, broad absorption with narrow and symmetric spectra and easy association with the other molecular groups [4]. The semiconductor nanocrystals have been used as fluorescent probes and as active components in nanotechnology-biomolecule complexes for biosensor applications [5,6].

In recent years, quantum dots have been used for biosensing due to the electrochemical as well as optical properties [8,9]. The bare quantum dots have been used with the principle of fluorescence resonance energy transfer (FRET) and photo-luminescence (PL) quenching technique to design biosensing assay system for the determination of glucose [10], and the capped QDs have been synthesized in a stable aqueous medium and this system has been used as a fluorescence probe for the mercury ions wherein the optimum fluorescence intensity is proportional to the ion concentration [11]. Furthermore the functional quantum dots have recently been introduced for molecular sieves sensors application [12]. Since, the majority of biosensing applications of quantum dots have been focused using their optical properties and very few results for quantum dots modified electrochemical sensors have been reported till date. Modifying the electrodes by the incorporation of quantum dots promotes direct electron transfer between the biomolecules and electrode surface [13], and also the direct electrochemistry has been reported by preparing the quantum dots/CNT electrode [7].

Among the various quantum dots cadmium sulphide (CdS) (band gap of 2.4 eV) has been studied with its excellent photoelectrochemical and optical properties [14-16]. Conjugated polymers specially like polyaniline combined with semiconductor nanoparticles (CdS, CdSe and TiO2) are widely studied with the remarkable physical, optical, electronic and photoelectric properties [17,22,24]. It has been observed that introducing nanocrystalline CdS on polymer enhances the charges on polymer backbone thus resulting conformational changes in structure of PANI which becomes expanded from its compact coiled form [18]. PANI-CdS composite not only exhibits the enhanced photo and electrical activity but it also increases the life of polymer and have good stability in ambient condition [21,23]. These properties of polymer-nanocrystal composite have led to increased interest to explore this PANI-CdS composite for biosensing purpose. Therefore on this way we have devised a novel electrode of PANI-(CdS-QD) composite for biosensing application.

Herein, we report results of the studies relating to the fabrication of PANI-(CdS-QD)/ITO electrode by electrochemical polymerization technique. The composite electrode is shown to have improved response as well as electrochemical stability due to in situ formation

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Experimental Section

Materials and reagents

Cholesterol oxidase (ChOx, EC 1.1.3.6, from *Pseudomonas fluorescens*) with specific activity of 24 U mg⁻¹, potassium mono-hydrogen phosphate, potassium dihydrogen phosphate, N-hydroxysuccinimide (NHS), N-ethyl-N-(3-dimethylaminopropyl) carbodiimide) (EDC) has been purchased from Sigma–Aldrich (USA). Aniline was distilled before electropolymerization. Distilled water is from Millipore water purification system. Cadmium chloride (CdCl₂) and sodium sulfide (Na₂S) have been purchased from Fisher scientific qualizes fine chemicals. Pre-cleaned ITO plates have been used as substrates for the electrochemical deposition of PANI-(CdS-QD) composite.

Synthesis of CdS quantum dots

For the synthesis of CdS quantum dots, 87.4 mg CdCl₂ is dissolved in 50 ml methanol followed by sonication for about 10 mins. 7 mg Na₂S is dissolved in 5 ml methanol separately and sonicated. Now Na₂S solution is added into the CdCl₂ solution with continuous vigorous stirring till the solution turns yellow. The resultant solution is then centrifuged and powder of CdS quantum dots has been obtained.

Fabrication of H₂SO₄ doped PANI-(CdS-QD) electrode

PANI-(CdS-QD) composite film has been fabricated onto ITO glass plates by electrochemical deposition technique in a three electrode cell having Pt foil as counter electrode and Ag/AgCl as the reference electrode. The 50 µl distilled aniline, 0.5 ml H₂SO₄ and 17.5 mg CdCl₂ are mixed in 9 ml double distilled water and the solution is placed in a three electrode glass cell for electrochemical treatment. Synthesis has been carried out in two steps, firstly a current of 60 µA has been kept constant for 300 s (schematic is shown in Figure 1). The electrode is then taken out and washed properly with distilled water. Again putting electrode into the shell and before starting the electro polymerization we injected 1.4 mg/ml solution of Na₂S into the cell which forms the suspensions of CdS nanoparticles in the mixture uniformly, and the similar treatment is done with 120 µA current for next 300 s for the formation of PANI-(CdS-QD) composite on ITO. After synthesis electrode is rinsed thoroughly in distilled water, dried and stored at 4°C.

Immobilization of Cholesterol oxidase (ChOx) onto electrodes

Cholesterol oxidase is covalently immobilized on the surface of prepared electrodes. For this purpose, 50 mg EDC and 10 mg NHS are mixed in 200 µl ChOx added with 400 µl distilled water. 30 µl of this solution is spread on the surface of prepared electrode and then left the electrode inside a humid chamber for about four hours for the proper immobilization of enzyme on electrode surface.

Photometric studies

Photometric experiments have been carried out as a function of cholesterol concentration using PBS buffer (50 mM, pH 7.4, 0.9% NaCl). These measurements have been made to estimate the enzyme activity, reproducibility and the interferent studies of the bioelectrode. To carry out photometric enzymatic assay of the immobilized ChOx, ChOx/PANI-(CdS-QD)/ITO bioelectrode has been dipped in 3 ml PBS solution containing 20 µl HRP (1 mg dl⁻¹), 20 µl o-dianisidine dye and 100 µl of cholesterol. The difference between the initial and final absorbance value at 500 nm after 3 min incubation of cholesterol has been recorded and plotted.

Instrumentation

Scanning electron microscopy (SEM, Zeiss EVO 40) and transmission electron microscopy (JEOl-2100F) have been used to reveal the formation of CdS-QD, PANI/ITO, PANI-(CdS-QD)
Results and Discussion

TEM analysis of CdS quantum dots

The morphology of the prepared CdS studied by the high resolution transmission electron microscopy (HRTEM) is shown in Figure 2. The existence of lattice planes clearly visible in the HRTEM image are indicative of crystallinity in CdS quantum dots. The TEM image shows the well dispersed CdS QDs and most of the dots have been examined to have the elliptical shape with diameter ranging from 4 to 7 nm. The inset shows the HRTEM image of a single quantum dot with clearly visible lattice planes having the inter-planar distance around 0.133 nm between the two consecutive planes.

UV-visible analysis

Figure 3 shows the UV-Vis absorption spectra of CdS quantum dots (i), PANI/ITO electrode (ii) and PANI-(CdS-QD)/ITO electrode (iii), respectively. In the UV-Vis spectra of CdS solution in methanol, the absorption shoulder peak at 450 nm is assigned to the optical transition of the “exciton” in the first excitonic state and the significant blue shift in this peak with respect to bulk CdS (520 nm) corresponds to the formation of CdS within the diameter range of 4-5 nm due to quantum confinement effect [25]. The absorption spectrum of PANI shows bands around 355 nm and 420 nm corresponding to the π-π* transition of the “exciton” in the first excitonic state and the significant broadening of this peak shows the interaction of CdS quantum dots with the –NH2 and –NH- groups of PANI. The FT-IR spectrum of the PANI-(CdS-QD) composite film exhibits enhanced quinoid (Q) band intensity with respect to benzenoid (B) band when compared to that of PANI without CdS. The observed changes reveal the richness of the composite with quinoid units that can be assigned to the interaction of positively charged -NH=C groups of quinoid units with the negatively charged skeleton of CdS quantum dots that are likely to promote the stabilization of the quinoid ring structure in PANI. The peaks around 1570 (60% N-H Bending, 40% C-N stretching) and 1657 (80% C=O stretching + 10% C-N stretching + 10% N-H Bending) in the FT-IR spectra of CdS-QDs/PANI-(CdS-QD)/ITO electrode reveals the successful immobilization of CdS quantum dots on this nanocomposite matrix.
SEM analysis

The scanning electron microscopic (SEM) images of PANI/ITO, PANI-(CdS-QD)/ITO, ChOx/PANI-(CdS-QD)/ITO are shown in the figure 5. Figure 5(i) shows uniform globular morphology of PANI/ITO film with globule diameter varies in the range of 200 nm to 500 nm. The incorporation of CdS-QD within PANI matrix results in the generation of homogenous, densely packed nano-globular morphology of PANI-(CdS-QD)/ITO film (Figure 5 (ii)). These nano-globules show deviation in the range of 20 to 70 nm revealing as if QDs are acting as templates during the electrochemical polymerization of PANI thus resulting in its nano-structured deposition. The immobilization of ChOx is indicated by the masking of the nano-porous morphology of PANI-(CdS-QD)/ITO electrode with bright shining light shade macro-structures clearly visible on uniform smooth topology of PANI-(CdS-QD) matrix (Figure 5 (iii)).

Electrochemical Characterization Studies

Electrochemical analysis of PANI/ITO and PANI-(CdS-QD)/ITO electrode has been done using cyclic voltammetry (CV) and electrochemical impedance spectroscopy (EIS). CV and EIS studies have been carried out using a three-electrode cell with platinum foil as counter and Ag/AgCl as reference electrode in PBS (pH 7.0, 50 mM, 0.9% NaCl) on an Autolab Potentiostat/Galvanostat (Eco Chemie, Netherlands).

**CV Analysis:** To study the electrochemical behaviour, CV studies of PANI/ITO electrode and PANI-(CdS-QD)/ITO electrode have been investigated in the potential range of -0.5V to 0.5V at the scan rate of 50mVs$^{-1}$. The CV of PANI/ITO electrode shows redox behaviour with the anodic peak (0.05V) and cathodic peak (-0.2V) corresponds to the transition of PANI backbone from its leucoemeraldine state (reduced) to emeraldine state (partially oxidized). The CV of PANI-(CdS-QD)/ITO composite electrode in figure 6(A) reveals enhancement of the anodic and cathodic peak currents from 0.074 mA to 0.093 mA and from -0.115 mA to -0.147 mA, respectively, when compared to PANI/ITO electrode. This enhancement in the current is indicative of fast...
electron transport and increased charge transport in the parallel interface of electrolyte solution and PANI-(CdS-QD)/ITO electrode. This result can be attributed to the enhanced surface concentration of redox species (Γ) in the composite. To verify this, concentration of the redox species has been calculated using the Laviron’s equation [26] as given below

\[ E_{pa} = E^° + \frac{RT}{\alpha n F} \ln \left( \frac{RT}{\alpha n F} K_\alpha \ln \nu \right) \]

(1)

According to the above equation, the value of \( \frac{2.303RT}{\alpha n F} \), where \( \alpha \) is the transfer coefficient, \( F \) is the Faraday constant \((8.314 \text{ J mol}^{-1} \text{ K}^{-1})\), \( n \) is the number of electrons transferred and \( T \) is the temperature, for PANI/ITO and PANI-(CdS-QD)/ITO can be given by the slope of the plot of log scan rate (\( \nu \)) versus \( E_{pa} \) at different \( \nu \) values.

For PANI/ITO and PANI-(CdS-QD)/ITO electrodes, the anodic peak potential \( (E_{pa}) \) varies linearly with logarithm of \( \nu \) (scan rate, data not shown) and follows the equation 2nd & 3rd, respectively.

\[ E_{pa} \text{ (PANI/ITO)} = 0.092 \log \nu \text{ (Vs}^{-1}) + 0.0404; \text{ R = 0.92; SD = 0.0094} \]

(2)

\[ E_{pa} \text{ (PANI-(CdS-QD)/ITO)} = 0.1127 \log \nu \text{ (Vs}^{-1}) + 0.0348; \text{ R = 0.996; SD = 0.00372} \]

(3)

Considering equation (1), (2) and (3), the value of \( \frac{2.303RT}{\alpha n F} \) for PANI/ITO and PANI-(CdS-QD)/ITO can be given as

\[ \frac{2.303RT}{\alpha n F} = 0.19192 \text{ (For PANI/ITO)} \]  

(4)

\[ \frac{2.303RT}{\alpha n F} = 0.92 \text{ (For PANI-(CdS-QD)/ITO)} \]  

(5)

The value of \( \frac{2.303RT}{\alpha n F} \) can be used to calculate the total surface concentration of the redox species (Γ) on PANI/ITO and PANI-SWCNT/ITO electrode by using equation given below

\[ I_p = \frac{n^2 F^2 Γ \nu A}{4RT} \]

(6)

where \( I_p/\nu \) can be calculated from the slope of \( I_p \) vs. \( \nu \) plot [27].

The total surface concentration of redox species is found to be \( 3.211 \times 10^{-5} \text{ mol m}^{-2} \) for PANI-(CdS-QD)/ITO composite electrode, which is \( \sim 16 \) times to that of concentration for PANI/ITO electrode \( (2.047 \times 10^{-6} \text{ mol m}^{-2}) \).

This increase in the redox species supports strong interactions between the negatively charged quantum structures of CdS with the aromatic structures of PANI that helps in uncoiling of the otherwise folded chains of PANI also supported by UV-V is spectroscopy. In the extended open conformation of PANI, it is likely that more number of exposed moieties are available for oxidation leading to enhanced faradic current. Figure 6 (B & C) shows CV of PANI/ITO and PANI-(CdS-QD)/ITO electrode recorded at different scan rates (40–110 mV/s).

![Figure 6](image-url)
s^{-1}). Careful examination shows that while moving towards higher scan rate, there is a shift of the anodic peak towards more positive peak potential and cathodic peak in the reverse direction in case of PANI/ITO electrode. However, negligible or no shift is observed in PANI-(CdS-QD)/ITO system which is one of the primary criteria for the system to be reversible. Besides this, anodic and cathodic peak currents ($I_{pa}$ and $I_{pc}$) show improved linear behaviour with respect to square root of scan rate ($\sqrt{v}$) in case of PANI-(CdS-QD) composite matrix (Regression coefficient ($r$) = 0.99) (inset of Figure 6(B)) than that of pure PANI matrix ($r$ = 0.975) (inset of Figure 6(C)) revealing that the electron-transfer processes are more diffusion controlled in case of PANI-(CdS-QD)/ITO electrode. The linear regression equations for PANI/ITO and PANI-(CdS-QD) electrode are given as Equation (7-10).

\begin{align}
I_{pa} (\text{PANI/ITO}) &= 0.014 \sqrt{v} \text{ (Vs}^{-1}) - 0.04; r = 0.975; SD = 0.0046 \\
I_{pc} (\text{PANI/ITO}) &= -0.00159 \sqrt{v} \text{ (Vs}^{-1}) + 0.0206; r = -0.985; SD = 0.0079 \\
I_{pa} (\text{PANI-(CdS-QD)/ITO}) &= 0.012 \sqrt{v} \text{ (Vs}^{-1}) + 0.0198; r = 0.99; SD = 0.00224 \\
I_{pc} (\text{PANI-(CdS-QD)/ITO}) &= 0.00166 \sqrt{v} \text{ (Vs}^{-1}) + 0.074; r = -0.996; SD = 0.0037
\end{align}

The above discussion indicates that the incorporation of CdS quantum dots not only enhances the charge transfer properties of PANI matrix but leads to overall improvement in the electrochemical behavior of the system.

**Electrochemical impedance spectroscopy (EIS) studies:** EIS studies have been done to further support the improved electrochemical response of PANI matrix on the incorporation of CdS-QDs. Figure 6(D) shows that, in spite of similar shapes of the two Nyquist plots there is remarkable decrease in the diameter of the semicircle (indicative of charge transfer resistance) for the PANI-(CdS-QD) composite film. The smaller semicircle indicates that the charge transfer resistance ($6.32 \text{ K}$) for PANI-(CdS-QD) composite film is nearly half to that of the PANI film (12.6 K). This enhanced charge transfer is likely to be due to the presence of hopping centres created by the semiconducting CdS-QD in the PANI matrix that helps in faster charge transfer via electrons from one polymer chain to the other and finally to the electrode (ITO) surface. Moreover, incorporation of QDs facilitate the open conformation of PANI resulting in easy charge transport.

**Response studies using cyclic voltammetric technique**

To show the potential application of observed enhanced
The electrochemical properties of the PANI-(CdS-QD) composite, amperometric response studies of fabricated ChOx/PANI-(CdS-QD)/ITO bioelectrode have been carried out using CV studies in PBS in the range from -0.5 to 0.5 V (Figure 7(A)). During the response measurement, an anodic peak is observed around 0.03 V in CV which shows continuous increase in its intensity with increasing cholesterol concentration. The anodic peak seen around 0.03 V corresponds to the oxidation of PANI integrated within the matrix, and its increase with increased cholesterol concentration suggests that ChOx gets electrically contacted by PANI-(CdS-QD) modified ITO electrode. It may be noted that no peak is observed relating to the oxidation of H_2O_2 in the range of 0.5 to 0.7 V indicating that there is direct transfer of electrons from the reduced ChOx enzyme to the PANI-(CdS-QD) matrix during the biochemical reaction. Figure 7(B) shows plot of anodic peak current at 0.03 V for ChOx/PANI-(CdS-QD)/ITO bioelectrode as a function of cholesterol concentration. It can be seen that ChOx/PANI-(CdS-QD)/ITO bioelectrode can detect cholesterol in the range of 50 to 500 mg\text{dL}^{-1} with detection limit of 47.9 mg\text{dL}^{-1} and response time of 20 s. The value of sensitivity calculated from linear region of the calibration curve is 2.63 × 10^{-5} mA mg^{-1}\text{dL}^{-1}, with linear regression coefficient (r) as 0.995. The equation for the line of regression is given by:

\[
\text{Current (mA)} = 0.0247 \text{mA} + [2.63 \times 10^{-5} \text{mAmg}^{-1}\text{dL}^{-1}] \times [\text{Cholesterol Conc (mgdL}^{-1})]
\]

This high sensitivity of 2.63 × 10^{-5} mAmg^{-1}\text{dL}^{-1} and low response time of 20 s reveals enhanced bioelectrocatalytic activity of the enzyme on PANI-(CdS-QD)/ITO electrode due to the enhanced charge transfer properties of the composite matrix.

The apparent Michaelis-Menten kinetic parameter (\(K_{app}^m\)) of the enzymatic reaction, that determines the affinity of enzyme with the bioanalyte, has been estimated using Hanes plot i.e. a plot between analyte concentration [S] and [S]/Current (Figure 7(C)). The \(K_{app}^m\) value for the immobilized enzyme has been estimated to be 10 x 10^{-3} U cm^{-2}. The observed lower value of \(K_{app}^m\) shows enhanced affinity of the enzyme with the cholesterol in this nanocomposite matrix. Moreover, the PANI-(CdS-QD) matrix prepared by electrochemical technique may be helping the immobilized enzyme to achieve better conformation for faster enzymatic reaction resulting in enhancement of enzymatic activity.

**Photometric studies of ChOx/PANI-(CdS-QD)/ITO bioelectrode using UV-Vis technique**

Figure 8(A) shows photometric response of the ChOx/PANI-(CdS-QD)/ITO bioelectrode as a function of cholesterol concentration. The value of absorbance has been found to increase with increased cholesterol concentration [50-500 mgdL^{-1}]. The results have been utilized to estimate the amount of immobilized enzyme units using equation \(a_{app}^m\) (U cm^{-2}) = AV/\epsilon ts, where \(A\) is difference in absorbance before and after incubation, \(V\) is the total volume (3.14 cm^3), \(\epsilon\) is the millimolar extinction coefficient (7.5 for o-dianisidine at 500 nm), \(t\) is the reaction time (min) and \(s\) is the surface area (1 cm^2) of the electrode. The value of immobilized ChOx units was estimated to be 10 x 10^{-3} U cm^{-2}, indicating that 10 x 10^{-3} U cm^{-2} units of enzyme actively participate in the biochemical reaction.

Figure 8(B) shows the effect of interferents on the observed response of ChOx/PANI-(CdS-QD)/ITO electrode. In this figure, the first bar (cholesterol) shows the change in absorbance obtained with 200 mgdL^{-1} of cholesterol when compared with absorbance obtained for 0 mM of cholesterol concentration. The remaining bars show the absorbance corresponding to the mixture of cholesterol and interferents in 1:1 ratio. The straight line parallel to X-axis shows the variation in the presence of desired interferents, revealing a maximum of 6% interference. Studies revealed that the ChOx/PANI-(CdS-QD)/ITO bioelectrode retains more than 90% of activity even after 7 weeks (data not shown) and has reusability of about 9 times. Table 1 shows the comparison of present matrix to some of the other reported matrices for cholesterol detection.

**Conclusions**

We have successfully fabricated nanocomposite films of PANI and CdS-QD using electrochemical polymerization technique. The nanocomposite film deposition involves in-situ formation of CdS quantum dots that may act as templates for the aniline electro-polymerization and thus resulting in nanostructured PANI-(CdS-QD) film deposition on the indium-tin-oxide (ITO) coated glass plates. UV-Visible absorption study shows the increased charge species on the PANI backbone leads the transformation of PANI from its coiled conformation to the extended coil form. CV and EIS studies reveal fast charge transport (2 folds) in the PANI-(CdS-QD) system as compared to the analogous PANI system which is attributed to the enhanced surface concentration of redox species (~16 times) in the composite matrix. Moreover, the semiconducting CdS-QD provides 'hopping centres' that helps in the faster charge transfer via electrons from one polymer chain to the other and finally to the electrode surface. This
improved electrochemical behavior has been used to enhance the bioelectrocatalytic activity of the enzymes to obtain better biosensing characteristics. The response studies, carried out using CV technique, reveal that this CHx/PANI-(CdS-QD)/ITO bioelectrode can be used to detect cholesterol in the concentration range of 50 to 500 mg/dL with good detection limit (47.8 mg/dL) and low $K_{app}$ value (0.82 mM). This matrix can further be explored for the detection of other analytes (e.g. glucose, lactic acid, urea, antigens, antibodies etc.).

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Table 1: Characteristics of PANI-(CdS-QD) electrode along with those reported in literature for cholesterol detection.

| S. No. | Matrix                  | Linearity         | Sensitivity   | Response Time | Km app | Shelf Life | Reference                      |
|--------|-------------------------|-------------------|---------------|---------------|--------|------------|--------------------------------|
| 1      | Electrochemically deposited PANI | 100-400 mg/dl    | 0.042 µA/mg-m L^-1 | 240s          | 1.94   | 6 weeks    | [28]                           |
| 2      | MWNTs                   | 19.3-231.6 mg/dl  | 0.558µA cm^-2 mM^-1 | -            | 7.71   | -          | [29]                           |
| 3      | MWCNT/Screen Printed Carbon Electrode | 99.5-399 mg/dl   | 0.0059 µA/mg-m L^-1 | -            | -      | 9 weeks    | [30]                           |
| 4      | Gold electrode          | 0-80 mg/dl        | 0.13 µA/mM    | 15 s          | 2.94   | -          | [31]                           |
| 5      | ZnO Nanoparticles       | 0.001 – 0.5µM     | 23.7µAµM/M    | -            | 4.7    | -          | [32]                           |
| 6      | Chitosan-SnO nanocomposite | 0.26-10.36 mM  | 34.7 µA/mg-m L^-1 cm^-2 | -         | 3.8    | 12 weeks   | [33]                           |
| 7      | PANI-(CdS-QD) Nanocomposite | 50-500 mM        | 2.63 x 10^3 mA mg^-1 dL^-1 | 20s         | 0.82   | 7 weeks    | Present Work                  |

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