CT Attenuation Analysis of Carotid Intraplaque Hemorrhage

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ABSTRACT

BACKGROUND AND PURPOSE: Intraplaque hemorrhage is considered a leading parameter of carotid plaque vulnerability. Our purpose was to assess the CT characteristics of intraplaque hemorrhage with histopathologic correlation to identify features that allow for confirming or ruling out the intraplaque hemorrhage.

MATERIALS AND METHODS: This retrospective study included 91 patients (67 men; median age, 65 ± 7 years; age range, 41–83 years) who underwent CT angiography and carotid endarterectomy from March 2010 to May 2013. Histopathologic analysis was performed for the tissue characterization and identification of intraplaque hemorrhage. Two observers assessed the plaque’s attenuation values by using an ROI (≥ 1 and ≤2 mm²). Receiver operating characteristic curve, Mann-Whitney, and Wilcoxon analyses were performed.

RESULTS: A total of 169 slices were assessed (59 intraplaque hemorrhage, 63 lipid-rich necrotic core, and 47 fibrous); the average values of the intraplaque hemorrhage, lipid-rich necrotic core, and fibrous tissue were 17.475 Hounsfield units (HU) and 18.407 HU, 39.476 HU and 93.128 HU, respectively, before and after the administration of contrast medium. The Mann-Whitney test showed a statistically significant difference of HU values both in basal and after the administration of contrast material phase. Receiver operating characteristic analysis showed a statistical association between intraplaque hemorrhage and low HU values, and a threshold of 25 HU demonstrated the presence of intraplaque hemorrhage with a sensitivity and specificity of 93.22% and 92.73%, respectively. The Wilcoxon test showed that the attenuation of the plaque before and after administration of contrast material is different (intraplaque hemorrhage, lipid-rich necrotic core, and fibrous tissue had P values of .006, .0001, and .018, respectively).

CONCLUSIONS: The results of this preliminary study suggest that CT can be used to identify the presence of intraplaque hemorrhage according to the attenuation. A threshold of 25 HU in the volume acquired after the administration of contrast medium is associated with an optimal sensitivity and specificity. Special care should be given to the correct identification of the ROI.

ABBREVIATIONS: Az = area under the receiver operating characteristic curve; CEA = carotid endarterectomy; HU = Hounsfield unit; IPH = intraplaque hemorrhage; LRNC = lipid-rich necrotic core

During the past few years, several studies have demonstrated that the occurrence of intraplaque hemorrhage (IPH) in the carotid artery is linked with an increased risk of plaque rupture, and therefore, IPH is considered a fundamental parameter of the so-called plaque vulnerability. Most of the research performed in the past 20 years was based on results from autopsy studies or on the specimens taken from carotid endarterectomies. With the introduction of high-resolution black-blood MRI, it has become possible to identify non-invasively the IPH with optimal correlation to histology, and past literature has suggested an association between IPH and the occurrence of cerebrovascular events. In a recently published meta-analysis by Saam et al, it was demonstrated that the presence of IPH is associated with a 5- to 7-fold higher risk of cerebrovascular events.

However, carotid arteries are frequently imaged by using CT, which allows for characterizing the degree of stenosis with an excellent level of detail. Further, it offers information related to the risk of the plaque vulnerability such as the volume of the
plaque and its subcomponents or the identification of ulcers in the plaque. Moreover, CT provides a unique option in some categories of patients who cannot be imaged by using MR imaging (eg, those with a prosthetic valve). Therefore, the identification of the determinants of plaque vulnerability, and in particular IPH, could be extremely important.

The purpose of this study was to assess the CT characteristics of the IPH with histopathologic correlation to identify features that allow for confirming or ruling out the IPH.

MATERIALS AND METHODS

Study Design and Patient Population

The institutional review board of our hospital (Azienda Ospedaliera Universitaria di Cagliari) approved this retrospective study protocol, and we included all the patients who underwent carotid endarterectomy (CEA) and whose carotid specimen was analyzed by histologists. Therefore, 91 patients (67 men; median age, 65 ± 7 years; age range, 41–83 years) who underwent CEA from March 2010 to May 2013 were included. This research was conducted in accordance with the guidelines of our institution’s research committee, and because of the retrospective nature of the analysis, patient consent was waived.

We considered as an inclusion criterion that the CEA was performed within 10 days after the CTA, whereas we excluded those patients who underwent CEA for restenosis or radiation therapy–induced carotid stenosis. A further exclusion criterion was the plaque’s rupture or fragmentation during the CEA procedure and/or manipulation.

In our hospital, the quantification of the degree of stenosis and the carotid artery plaque analysis is performed by using CTA according to previously published inclusion criteria. Carotid sonography is used as the first-line technique to assess the presence of atheroma, and briefly, CTA of carotid arteries is performed when 1) carotid sonography shows a pathologic stenosis (> 50% measured with the NASCET criteria) or features related to plaque vulnerability (eg, ulcerations, irregular surface) and 2) sonography cannot adequately assess the degree of stenosis and the plaque’s characteristics because of anatomic conditions. Patients were also classified as symptomatic or asymptomatic according to the neurologic assessment documented in the clinical chart review by using the Trial of ORG 10172 in Acute Stroke Treatment (TOAST) criteria. Part of the study population (n = 58) of this research was included in previously published papers.

CTA Technique

Patients were studied by using a 16-multidetector row CT system (Brilliance; Philips Healthcare, Best, the Netherlands). CT images were obtained with coverage from the aortic arch to the carotid siphon with caudocranial direction. Examinations were performed before and after the administration of contrast material. Angiographic phase was obtained with the administration of 80 mL of prewarmed contrast medium (Ultravist 370; Bayer Healthcare, Berlin, Germany). CT technical parameters included: slice thickness, 0.6 mm; interval, 0.3 mm; matrix size, 512 × 512; and field of view, 14–19 cm. A C-filter algorithm of reconstruction was applied.

Carotid Endarterectomy

Two vascular surgeons (R.M. and R.S., with 25 and 16 years of experience, respectively) performed all the CEA procedures by using the “en-bloc” technique by scoring the outer media and adventitia with a scalpel and then removing the plaque as an intact tube. This approach was adopted to reduce the manipulation of the carotid artery and avoid the potential rupture/fragmentation of the plaque.

In our hospital, patients underwent CEA according to the recommendations by the Asymptomatic Carotid Atherosclerosis Study (ACAS), NASCET, Stroke Prevention and Educational Awareness Diffusion (SPREAD), and European Carotid Surgery Trial (ECST) after the exclusion of a cardioembolic source of embolism.

Histologic Analysis of the Plaque

The methods used for the plaque processing and histologic analysis have been described in a previously published paper. In summary, the histologic analysis was performed by 2 histologists (G.F. and L.L., with 22 and 5 years of experience, respectively) who were blinded to the radiologic findings. After the CEA, the excised “en-bloc” plaque is immediately fixed in formalin, and it is sent to the laboratory directly after the surgical procedure. Carotid plaques were decalcified and embedded in paraffin wax. None of the CEA specimens showed disruption of the luminal surface of the plaque. The portion of the specimen that showed the carotid plaque was divided transversely in sections having 3 mm intervals that were air-dried at 60°C for 45 minutes. After this phase, paraffin was removed by xylol, and the sections were hydrated. Finally, endogenous peroxidase activity was blocked by 2% hydrogen peroxide (H₂O₂). The transverse sections were subjected to histologic examination to identify the plaque components. Because the main focus of the study was to assess the attenuation characteristics of IPH, special care was used in the identification of IPH. Finally, according to the histologic characteristics, the plaque of each slice was categorized into one of 4 groups: IPH, lipid-rich necrotic core (LRNC), fibrous, and calcified.

Co-Registration and Histology Matching

The co-registration between CTA and histologic slices represents a key point of this paper, and special care was dedicated to avoid misregistration. After the selection of the CTA slice, the corresponding histologic section was identified by considering the following parameters: distance from the carotid bifurcation, lumen shape, and presence of prominent areas of calcification. In particular, the location of the bifurcation was identified to measure the length in the z-axis correctly. Moreover, given the difference in thickness between the MDCTA image sections (0.625 mm) and the histologic cross sections (5 μm), to further validate, 2–3 histologic sections were compared with 1 cross-sectional MDCTA image on the basis of the relative distance from the bifurcation.
In this study, the registration phase between CT and histologic slices was fundamental, and special care was used. The CT analysis was performed in 3 different phases. The first one was conducted with both radiologists in consensus to assess the image quality of the datasets and exclude those carotid arteries that showed dental streak artifacts or movement artifacts that reduced the image quality. The second and third phases were performed with radiologists who worked independently.

In the second phase, the angiographic dataset was assessed; radiologists had histopathologic sections as well as the spatial coordinates (slice number – Z distance from the carotid bifurcation), and they were asked to trace a circular or elliptical ROI (≥ 1 mm² and ≤2 mm²) in the plaque and to quantify the HU attenuation values in the analyzed slice. The shape of the vessel wall and the lumen as well as the location of the bifurcation and the presence of calcifications in the plaque were used for matching. The procedures were repeated for each slice of each patient where it was possible to trace an ROI of at least 1 mm².

In the third phase, radiologists selected the basal scan dataset and identified the same slice corresponding to the angiographic phase. To reach a correct registration between basal and angiographic datasets, they visually verified if the slices were registered or if it was necessary to select another slice along the z-axis. After this “matching phase,” the same ROI used in the contrast phase (duplicate option) was positioned in the same position of the plaque to measure the attenuation values (Fig 1).

**Statistical Analysis**

In this study, the normality of each continuous variable group was tested by using the Kolmogorov-Smirnov Z test, and appropriate tests for Gaussian or non-Gaussian values were selected. The Bland-Altman plot was calculated between the 2 readers to test the attenuation values, and the averaged value for each section was considered for the analysis. The Mann-Whitney test was calculated to test the difference of attenuation values between the different categories (IPH, LRNC, and fibrous tissue). Receiver operating characteristic curve analysis was performed, and the model was characterized by the area under the receiver operating characteristic curve (Az) with 95% CIs to test the relationship between HU attenuation values in the ROI and IPH. Moreover, thresholds derived from the ROC analysis were calculated. The Wilcoxon test was applied to test the difference of attenuation values before and after administration of contrast material for the plaques (IPH, LRNC, and fibrous).

A *P* value <.05 was regarded as indicating a statistically significant association, and all values were calculated by using a 2-tailed significance level. R statistical and computing software (www.r-project.org) was used for statistical analyses.

**RESULTS**

**General Results**

The mean time interval between CT and CEA was 9 days (range, 3–14 days). No patients were excluded from the analysis. Twenty-six cases of IPH were found (prevalence of 23.08%), and another 21 had LRNC without IPH (prevalence 23.07%). In 5 cases, along the length of the plaque, there were histologic slices with LRNC and other slices with IPH (prevalence of 5.45%). The other 39 plaques did not show IPH or LRNC and were mainly calcified (*n* = 24) or characterized by fibrous tissue or myofibroblast proliferation (*n* = 15).

In our cohort, we found 29 asymptomatic patients and 62 symptomatic patients. (In the 62 symptomatic patients, 25 strokes, 24 transient ischemic attacks, and 13 cases of amaurosis fugax were observed.) The analysis of the association between IPH and...
Therefore, the identification of values between −4 HU and +5 HU for LRNC, and between −6 HU and +12 for fibrous tissue.

**Mann-Whitney Test**

By comparing the attenuation values among the 3 different analyzed categories (IPH, LRNC, and fibrous), we found that there was a statistically significant difference of HU values both before and after the administration of contrast material (Table 2). In Fig 2 a boxplot shows the attenuation values according to the category.

**Receiver Operating Characteristic Curve Analysis**

The receiver operating characteristic curve analysis was performed to test the association between the HU attenuation and the presence or absence of IPH, shown in Fig 3. The Az for the attenuation analysis performed in the basal scan was 0.944, whereas the Az after the administration of contrast medium was 0.978 (difference between the Az; P = .026). From the receiver operating characteristic curve analysis, we also tested multiple thresholds to identify the best combination of sensitivity and specificity value (Table 3). We found that a threshold of 25 HU in the plaque (in the dataset after administration of contrast material) has a sensitivity of 93.22% and a specificity of 92.73% for the presence of IPH.

**Wilcoxon Analysis**

This test was used to check the effect of the contrast material in the plaque categories. By comparing the overall attenuation of the plaques (IPH, LRNC, and fibrous) before and after the administration of contrast medium, we found a statistically significant difference (P = .001). By assessing the attenuation of IPH, LRNC, and fibrous tissue before and after contrast medium, we found P values of .006, .0001, and .018, respectively, demonstrating that the attenuation of the plaque before and after administration of contrast material is different.

**DISCUSSION**

Recent published studies have demonstrated that the presence of IPH is related to an increased risk of stroke independent of the severity of luminal stenosis. Therefore, the identification of IPH represents an important step to correctly stratify the risk of potential cerebrovascular events of a subject.

CT is a widely used technique for the preoperative assessment of the subject, which allows for obtaining information related to other features related to the plaque’s vulnerability such as the presence of ulcerations or large plaque volume. It is important to remember that because of the radiation delivered, CT is not considered the best tool for follow-up of patients with carotid artery stenosis (unlike ultrasound), and that is one of its main limitations as a diagnostic tool; however, the improvement in CT technology with the introduction of dose-reduction techniques results in a viable option. The purpose of this study was to assess the CT characteristics of IPH with histopathologic correlation to identify features that allow for confirming or ruling out the IPH.

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### Table 1: Summary of attenuation values

| Type of Tissue | N   | Mean HU | SD  | Median | 2.5–97.5 Percentiles | Normal Distribution |
|---------------|-----|---------|-----|--------|----------------------|---------------------|
| **Basal**     |     |         |     |        |                      |                     |
| Fibrous       | 47  | 91.66   | 17.7474 | 93   | 47.525–121.400       | 0.0052              |
| LRNC          | 63  | 39.476  | 19.4529 | 34   | 16.075–87.625        | 0.0355              |
| IPH           | 59  | 17.475  | 4.9283  | 17   | 8.975–26.025         | 0.0668              |
| **Contrast**  |     |         |     |        |                      |                     |
| Fibrous       | 47  | 93.128  | 16.3609 | 94   | 49.875–120.775       | 0.0003              |
| LRNC          | 63  | 48.048  | 19.3811 | 43   | 21.000–85.925        | 0.1446              |
| IPH           | 59  | 18.407  | 4.8428  | 18   | 10.975–27.000        | 0.0021              |

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### Table 2: Mann-Whitney analysis

| Type of Tissue | IPH   | LRNC  | Fibrous |
|---------------|-------|-------|---------|
| **Basal**     |       |       |         |
| IPH           | x     | 0.001 | 0.001   |
| LRNC          | 0.001 | x     | 0.001   |
| Fibrous       | 0.001 | x     | x       |
| **Contrast**  |       |       |         |
| IPH           | x     | 0.001 | 0.001   |
| LRNC          | 0.001 | x     | 0.001   |
| Fibrous       | 0.001 | x     | x       |

Note: —x indicates test is not applicable.
To obtain correct data, our readers (histologists and radiologists) gave special attention to excluding all those slices or CT datasets that were not optimal from a technical point of view. Moreover, the calcified plaques or those plaques with a visible cluster of calcium were excluded. First, the identification of the calcium is extremely easy thanks to the big attenuation that this tissue produces in the x-rays. For the same reason, those histologic slices where calcium was visible in small amounts were excluded. From the original 435 histologic slices, radiologists analyzed 169 slices (38.9%).

We found that the average value of the IPH was extremely low, with an average basal value of 17.475 HU and average value of 18.407 HU after the administration of contrast medium. In 2009, Adjuk et al\textsuperscript{28} found that the attenuation values of the American Heart Association plaque VIb (confluent extracellular lipid core complicated by hemorrhage) was lower compared with the other types of plaque, with an average value of 22 HU compared with 59 HU for the other types of plaques, and these data were confirmed in a further publication performed by the same group in 2013.\textsuperscript{29} Our values are lower compared with those found by Adjuk et al,\textsuperscript{28,29} and we think that this can be attributed to 2 different causes. First, the different selection criteria; in fact, we excluded all those plaques that also had a small cluster of calcium that can justify the raised attenuation values in the work of Adjuk et al.\textsuperscript{28,29} Second, we did not considered histologic slices with LRNC and IPH, but only those 2 features independently; this approach may explain the lower attenuation values of our observations. In addition, a study published by de Weert et al\textsuperscript{30} in 2006 demonstrated that the presence of very hypoattenuated areas was associated with the presence of plaques complicated by hemorrhage (<30 HU).

We also compared the attenuation values among the 3 different analyzed categories (IPH, LRNC, and fibrous), and we found that there was a statistically significant difference of HU values (Table 2). This result demonstrates that the attenuation values are different from the attenuation of LRNC and fibrous tissue. In particular, hemorrhage has significantly lower attenuation values compared with the other categories of tissues.

The receiver operating characteristic curve analysis confirmed the strength of the association between the hypoattenuated values and presence of IPH (Az = 0.944 in basal analysis and 0.978 after contrast medium), and by considering a threshold value of 25 HU (in the scans obtained after the administration of contrast material), we obtained a sensitivity of 93.22% and a specificity of 92.73% for the presence of IPH. These results demonstrated that it is possible to identify an attenuation threshold by identifying the presence of IPH.

Our results are different from those observed by U-King-Im et al\textsuperscript{31} where the authors compared CTA and IPH detected by MR imaging and found that mean CT plaque attenuation was higher for plaques with MR imaging–defined IPH (47 HU) compared with plaques without IPH (43 HU). Moreover, they found a significant overlap between the distributions of plaque densities by concluding that mean plaque attenuation is of limited value in distinguishing between the 2 groups. The differences between our results and the paper by U-King-Im et al\textsuperscript{31} can be explained by the different methodology applied. They used as reference standard MR-defined IPH, whereas we considered the histopathologic

**FIG 2.** Boxplot with the attenuation values before and after the administration of contrast material according to the type of tissue.

**FIG 3.** Receiver operating characteristic curve analysis that shows the Az of the attenuation (basal and after the administration of contrast medium) versus the presence/absence of IPH.

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slices. We excluded from the analysis all the slices where a cluster of calcium was identified, and this explains the average lower CT values found in our study in those plaques with IPH. Moreover, we considered multiple sections for each plaque according to the histopathologic category, and this is important because we found 10 plaques where there were areas with IPH and others without IPH. These findings confirm that in the same plaques, there exist different tissues, and they are not always represented in a single axial section. For this reason, we suggest readers check the entire length of the plaque and not only the thickest point and assess with ROIs having different levels of the plaque. This is a significant point because the plaques show a spatial heterogeneity other than a temporal variability; therefore, the plaque should be considered a dynamic process, and lack of IPH doesn’t mean that sometime in the future IPH cannot appear.

We also tested the difference in attenuation before and after the administration of contrast medium and found that there was a statistically significant difference (.006, .0001, and .018 for IPH, LRNC, and fibrous tissue, respectively), by confirming the fact that the contrast material plays an important role in the attenuation values of the carotid artery plaques.32-34

In this study, there are some limitations. First, this is a retrospective study, and this approach may determine a bias; however, it is our opinion this can be considered a minor limitation because our focus was to assess the attenuation value of the IPH, and we would use the same paradigm in prospective approach. Second, the registration between histologic sections and the CT dataset is fundamental to obtain correct as well as relevant data. We tried to use our experience and all the potential tools to overcome the problems related to the registration (spatial registration features, manual and experienced correction, and the use of 2 different readers). However, there are some limits that are not possible to solve, in particular, the fact that the histologic preparation leads to plaque shrinkage33; in the study by de Weert et al.,30 the total plaque area acquired in MDCTA images was 30% larger than the histologic total plaque area.

CONCLUSIONS
The results of this preliminary study suggest that CT can be used to identify the presence of IPH according to the attenuation. A threshold of 25 HU in the volume acquired after the administration of contrast medium is associated with an optimal sensitivity and specificity. Special care should be given to the correct identification of the area to place the ROI.

Disclosures: Marco Francone—UNRELATED: Payment for Lectures Including Service On Speakers Bureau: Bracco Medical Imaging. Carlo Nicola De Cecco—UNRELATED: Grants/Grants Pending: Siemens.* *Money paid to the institution.

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Table 3: Threshold analysis

| HU Value | Sensitivity | Specificity | +LR | -LR | Sensitivity | Specificity | +LR | -LR |
|----------|-------------|-------------|-----|-----|-------------|-------------|-----|-----|
| <0       | 0.00        | 100.00      | NC  | 1.00| 0.00        | 100.00      | NC  | 1.00|
| ≤2       | 55.93       | 96.46       | 11.1 | 0.64| 35.39       | 100.00      | NC  | 1.00|
| ≤4       | 67.52       | 93.64       | 17.1 | 0.64| 45.76       | 99.66       | 18.64| 0.32|
| ≤8       | 64.99       | 93.58       | 14.6 | 0.27| 67.80       | 95.58       | 16.41| 0.27|
| ≤12      | 71.19       | 90.00       | 10.2 | 0.27| 76.27       | 95.58       | 16.78| 0.25|
| ≤16      | 77.97       | 90.00       | 7.72 | 0.27| 81.36       | 93.64       | 12.82| 0.20|
| ≤20      | 84.75       | 84.55       | 5.48 | 0.34| 93.22       | 92.73       | 12.82| 0.073|
| ≤22      | 88.14       | 83.84       | 5.39 | 0.073| 100.00      | 92.73       | 13.75| 0.00|
| ≤25      | 94.92       | 83.64       | 5.80 | 0.061| 100.00      | 92.73       | 13.75| 0.00|
| ≤30      | 100.00      | 80.91       | 5.24 | 0.00| 100.00      | 92.73       | 13.75| 0.00|
| ≤120     | 100.00      | 0.00        | 1.00 | NC  | 100.00      | 0.00        | 1.00 | NC  |

Note: +LR indicates positive likelihood ratio; −LR, negative likelihood ratio; NC, not classifiable.
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