Development and Evaluation of Floating Sustained Release Bilayer Tablets Containing Dothiepin HCl

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ABSTRACT

Bilayer floating tablets of Dothiepin HCL were developed by direct compression method. Immediate release layer contains 30 mg of drug and super disintegrant sodium starch glycolate, serves the purpose of loading dose. Sustained release layer contained HPMC K4M, natural polymers like xanthan gum, guar gum, karaya gum release the drug for 12 hours’ time. Sodium bicarbonate and citric acid are used to produce effervescence. Floating lag time of optimized tablet is 92 sec, whereas floating duration is more than 12 hours. FTIR results revealed that there was no interaction between drug and HPMC K4M / xanthan gum. The post compression parameters of developed tablets were found to be satisfactory. In this study, it was confirmed that the formulations containing HPMC K4M, have shown better floating properties and finally the formulation containing a combination of HPMC K4M and xanthan gum in 3:1 ratio, has exhibited decent sustained drug release properties. The release kinetics of optimized formulation prepared with the combination of HPMC K4M and xanthan gum followed zero order kinetics.

Keywords: Floating Bilayer Tablet, Dothiepin HCL, HPMC K4M, Xanthan Gum, FTIR.

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INTRODUCTION

Oral route is the most preferred route for administration of drugs. Tablets are the most popular oral formulations available in the market and preferred by the patients and physicians alike. In long term therapy for the treatment of chronic disease conditions, a conventional formulation is required to be administered in multiple doses, and therefore lacks patient compliance [1]. Sustained release tablet formulations are much desirable and preferred for such therapy because they offer better patient compliance, maintain uniform drug levels, reduce dose, and side effects, and increase safety margin for high-potency drugs [2]. Oral drug delivery continues to rise in popularity as formulation scientists look for ways to control drug release and improve patient convenience. However, developing oral sustained release tablets for water soluble drugs with constant release rate has always been a challenge to the pharmaceutical technologist. Most of these water-soluble drugs if not formulated properly, may readily release the drug at a faster rate and produce a toxic concentration of drug on oral administration [3].

In the last decade, interest in developing a combination of two or more Active Pharmaceutical Ingredients (API) in a single dosage form (bilayer tablet) has increased in the pharmaceutical industry, promoting patient convenience and compliance. Bilayer tablets allows for designing and modulating the dissolution and release characteristics [4]. The term bilayer tablets containing subunits that may be either the same (homogeneous: one layer of drug for immediate release while second layer for sustained release) or different (heterogeneous: sequential release of two drugs in combination or separate two incompatible substances) [5]. The important advantages of bilayer tablets are ability to combine different release rate IR and SR in the same tablet for chronic condition requiring repeated dosing; retain potency and ensure dose accuracy; blood level of a drug can be held at consistent therapeutic level for improved drug delivery, accuracy and safety; reduction of adverse effects [6, 7].

Dothiepin HCL (Figure 1) is a bicyclic antidepressant and is usually categorized as a serotonin norepinephrine reuptake inhibitor (SNRI), but it has been referred to as a serotonin norepinephrine-dopamine reuptake inhibitor (SNDRI). It works by blocking the transporter "reuptake" proteins for key neurotransmitters affecting mood, thereby leaving more active neurotransmitters in the synapse [8]

MATERIALS AND METHOD

The chemicals used in this study were pure drug like Dothiepin HCL (Yarrow chemicals) and polymers like HPMC K4M, Xanthan gum, Guar gum, Karaya gum, Locust bean gum and other
excipients like micro crystalline cellulose, magnesium stearate, talc, sodium bicarbonate, citric acid (Yarrow chemicals).

**Pre-formulation Study:**
Pre-formulation studies were conducted to confirm the compatibility of drug with polymers used. These studies were conducted by using FTIR spectrophotometer. In this method, the IR spectra of pure drug, physical mixtures containing drug and polymers (1:1) and tablet triturate were analyzed.

**Evaluation of Flow Properties:**
Prepared powder blend of the different formulations were evaluated for angle of repose, loose bulk density, tapped bulk density and compressibility index.

**Preparation of Floating Bilayer Tablets:**
The drug and excipients for immediate release layer mentioned in Table-1 were passed through a 60 # size mesh prior to the preparation of the dosage form. All the ingredients sufficient to produce 20 tablets are weighed separately and mixed thoroughly for 10 min the mixture of first layer was subjected to slight compression to using ten station rotary tablet machines.

Drug and excipients for sustained release layer mentioned in Table-2 were passed through a 60 # size mesh prior to the preparation of the dosage form. All the ingredients where weighed separately and mixed thoroughly for 10 min. These mixtures is placed over the first layer and subjected for final compression to produce tablet with 6 ± 0.5 Kg/cm2 hardness. Bilayer tablet containing immediate release layer (IR) and sustained release layer (SR) is termed as formulations F1, F2 and so on.

Table 1: Formulation of sustained (SR) and immediate (IR) drug release layers of Dothiepin HCL bilayer tablet.

**Formulation for immediate release layer.**

| Ingredients              | Weight in (mg) |
|--------------------------|----------------|
| Dothiepin HCL            | 30             |
| Sodium starch glycolate  | 40             |
| MCC                      | 123            |
| Polyvinyl pyrrolidone   | 5              |
| Magnesium stearate      | 2              |
Table 2: Formulation for sustained release layer:

| Ingredients (mg)       | SR1 | SR2 | SR3 | SR4 | SR5 | SR6 | SR7 | SR8 | SR9 | SR10 | SR11 | SR12 | SR13 | SR14 | SR15 |
|------------------------|-----|-----|-----|-----|-----|-----|-----|-----|-----|------|------|------|------|------|------|
| Dothiepin HCL          | 120 | 120 | 120 | 120 | 120 | 120 | 120 | 120 | 120 | 120  | 120  | 120  | 120  | 120  | 120  |
| HPMC K4M               | 100 | ___ | ___ | ___ | ___ | 75  | 75  | 75  | 75  | 75   | 75   | 75   | 75   | 75   | 75   |
| Xanthan gum            | ___ | 100 | ___ | ___ | ___ | 25  | ___ | ___ | ___ | 12.5 | 12.5 | 12.5 | ___  | ___  | ___  |
| Guar gum               | ___ | ___ | 100 | ___ | ___ | 25  | ___ | ___ | ___ | 12.5 | ___  | 12.5 | 12.5 | ___  | ___  |
| Locust bean gum        | ___ | ___ | ___ | 100 | ___ | 25  | ___ | ___ | ___ | 12.5 | ___  | 12.5 | ___  | 12.5 | ___  |
| Karaya gum             | ___ | ___ | ___ | ___ | 100 | ___ | ___ | ___ | 25  | ___  | 12.5 | ___  | 12.5 | 12.5 | 12.5 |
| Citric acid            | 9   | 9   | 9   | 9   | 9   | 9   | 9   | 9   | 9   | 9    | 9    | 9    | 9    | 9    | 9    |
| Sodium bicarbonate     | 21  | 21  | 21  | 21  | 21  | 21  | 21  | 21  | 21  | 21   | 21   | 21   | 21   | 21   | 21   |
| MCC                    | 44  | 44  | 44  | 44  | 44  | 44  | 44  | 44  | 44  | 44   | 44   | 44   | 44   | 44   | 44   |
| Mg. Stearate           | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3    | 3    | 3    | 3    | 3    | 3    |
| Talc                   | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3   | 3    | 3    | 3    | 3    | 3    | 3    |
Evaluation:

Hardness test:
The Monsanto hardness tester was used to determine the tablet hardness. The tablet was held between a fixed and moving jaw. Scale was adjusted to zero; load was gradually increased until the tablet fractured. The value of the load at that point gives a measure of hardness of the tablet. Hardness was expressed in Kg/cm².

Friability test:
Tablet strength was tested by Roche friabilator. Pre-weighed tablets were allowed for 100 revolutions (4 min), taken out and were dedusted. The percentage weight loss was calculated by rewriting the tablets. The % friability was then calculated by,

\[ F = \frac{(W_{\text{initial}}) - (W_{\text{final}})}{(W_{\text{initial}})} \times 100 \]

Uniformity of weight:
20 tablets from each of the formulation were weighed individually with an analytical weighing balance (Model: AY-200, SHIMADZU Corporation, and JAPAN). The average weights for each brand as well as the percentage deviation from the mean value were calculated.

Drug content uniformity:
Accurately weighed quantity of the powder tablet equivalent to 20mg of the drug and 80mg of tablet powder was transferred to 100ml volumetric flask separately. 50ml of buffer solution of pH 6.8 was added. And then the volume was made up to 100ml with the same buffer solution, mixed solution was filtered through the membrane filter. 5ml of the filtrate was diluted to 50 ml with same buffer solution and examined under U.V. Spectrophotometry at 228 nm.

In Vitro Drug Release:
The release of Dothiepin HCL from floating tablets was determined by using dissolution type-II test apparatus. The dissolution test was performed using 900 ml 0.1N HCl solution at 37 ± 0.5°C temperature and at 50 rpm. At specified time intervals, samples of 5 ml were withdrawn from the dissolution medium and that amount was replaced with fresh medium to maintain the volume constant. The samples were filtered and diluted to a suitable concentration with 0.1 N HCl. The absorbance of the diluted samples was measured at 228 nm for Dothiepin HCL by using UV spectrophotometer. Cumulative percentage drug release was calculated using an equation obtained from standard curve. Dissolution test was continued for 12 hours using pH 6.8 phosphate buffer.
RESULTS AND DISCUSSION:

The standard graph of Dothiepin HCL has shown good linearity with $r^2$ value 0.997 in pH 6.8 buffer solution which suggests that it obeys the “Beer-Lambert’s law”.

FTIR:

Drug polymer interaction was checked by comparing the IR spectra of the formulations with the IR spectra of the pure drug. There was no significant change in the functional groups between the IR spectra of the pure drug and also no additional peaks were seen in the selected formulations. This confirms that no interaction between drug and excipients.

FTIR OF DRUG AND POLYMER INTERACTION:

![Figure 1: FT-IR of DOTHIIEPIN HCL](image1)

![Figure 2: FT-IR of DOTHIIEPIN HCL+HPMC K4M](image2)
Figure 3: FT-IR of DOTHIPEPIN HCL+XANTHAN GUM

Figure 4: FT-IR of DOTHIPEPIN HCL+GUAR GUM

Figure 5: FT-IR of DOTHIPEPIN HCL+KARAYA GUM
Evaluation of Bilayer Tablet:

The Dothiepin HCL tablet was evaluated for hardness, thickness, friability, weight variation and drug content uniformity. The hardness was in the range of 6.1 to 7.6 kg/cm², which was in accordance with the bi-layer tablet. The thickness was from 3.40 to 3.62 mm suggested uniformity in thickness for bi-layer tablet. The friability was less than 1% indicated good handling of the layers. The weight variation results suggested uniformity in weight of layers.
Table 3: Pre-compression parameters for Dothiepin HCL immediate release and sustained release layers.

| Batch Code | Bulk density (gm/cm$^3$) | Tapped density(gm/cm$^3$) | Carr’s index | Hausner Ratio | Angle of Repose (°) |
|------------|--------------------------|---------------------------|--------------|---------------|-------------------|
| SR1        | 0.476±0.05               | 0.545± 0.02               | 12.45±0.06   | 1.12±0.05     | 25.20±0.01        |
| SR2        | 0.568±0.04               | 0.651±0.02               | 14.33±0.04   | 1.18±0.06     | 22.56±0.02        |
| SR3        | 0.502±0.04               | 0.571±0.02               | 11.82±0.03   | 1.13±0.04     | 23.42±0.02        |
| SR4        | 0.515±0.07               | 0.595±0.03               | 13.95±0.04   | 1.15±0.04     | 24.40±0.02        |
| SR5        | 0.519±0.04               | 0.591±0.02               | 12.86±0.03   | 1.13±0.05     | 24.40±0.02        |
| SR6        | 0.499±0.02               | 0.582±0.04               | 12.08±0.02   | 1.15±0.08     | 23.10±0.03        |
| SR7        | 0.531±0.04               | 0.610±0.03               | 13.76±0.02   | 1.15±0.07     | 23.51±0.04        |
| SR8        | 0.532±0.03               | 0.591±0.03               | 14.25±0.03   | 1.13±0.05     | 24.42±0.02        |
| SR9        | 0.488±0.03               | 0.553±0.03               | 11.43±0.03   | 1.12±0.07     | 22.90±0.01        |
| SR10       | 0.568±0.04               | 0.651±0.02               | 14.33±0.04   | 1.18±0.06     | 22.56±0.02        |
| SR11       | 0.591±0.04               | 0.591±0.02               | 12.86±0.03   | 1.13±0.05     | 24.40±0.02        |
| SR12       | 0.531±0.04               | 0.610±0.03               | 13.76±0.02   | 1.15±0.07     | 23.51±0.04        |
| SR13       | 0.476±0.05               | 0.545±0.02               | 12.45±0.06   | 1.12±0.07     | 23.10±0.03        |
| SR14       | 0.515±0.07               | 0.595±0.03               | 13.95±0.04   | 1.15±0.04     | 24.40±0.02        |
| SR15       | 0.488±0.03               | 0.553±0.03               | 11.43±0.03   | 1.12±0.07     | 22.56±0.02        |

Post compressional parameters

Table 4: Post compressional parameters of Dothiepin HCL Bilayer tablets.

| Batch code | Hardness (kg/cm$^2$) | Thickness (mm) | Friability % | Weight Variation (mg) | Drug content % |
|------------|----------------------|----------------|--------------|-----------------------|----------------|
| F1         | 7.1±0.02             | 3.41±0.06      | 0.10±0.05    | 499.3±9.15            | 98.73±0.31     |
| F2         | 6.2±0.04             | 3.40±0.06      | 0.19±0.02    | 498.9±9.98            | 98.53±0.58     |
| F3         | 6.3±0.02             | 3.41±0.08      | 0.18±0.07    | 497.9±9.78            | 98.57±0.33     |
| F4         | 6.2±0.02             | 3.41±0.07      | 0.23±0.04    | 499.5±9.91            | 98.58±0.51     |
| F5         | 6.2±0.03             | 3.40±0.07      | 0.26±0.02    | 495.5±9.91            | 98.57±0.68     |
| F6         | 7.4±0.05             | 3.50±0.03      | 0.10±0.08    | 499.2±9.85            | 99.65±0.01     |
| F7         | 7.6±0.04             | 3.61±0.08      | 0.11±0.08    | 499.1±9.19            | 98.57±0.78     |
| F8         | 7.5±0.02             | 3.58±0.09      | 0.15±0.03    | 497.9±9.99            | 98.58±0.91     |
| F9         | 7.6±0.05             | 3.60±0.06      | 0.13±0.02    | 498.5±9.83            | 98.57±0.32     |
| F10        | 7.6±0.06             | 3.59±0.08      | 0.15±0.07    | 498.8±9.87            | 98.57±0.30     |
| F11        | 7.4±0.05             | 3.62±0.05      | 0.16±0.02    | 498.6±9.59            | 97.02±0.08     |
| F12        | 7.6±0.03             | 3.54±0.01      | 0.11±0.01    | 499.1±9.87            | 98.57±0.52     |
| F13        | 7.3±0.07             | 3.62±0.01      | 0.13±0.02    | 498.5±9.89            | 97.06±0.03     |
| F14        | 7.1±0.08             | 3.49±0.09      | 0.12±0.03    | 498.9±9.87            | 98.57±0.01     |
| F15        | 7.4±0.03             | 3.52±0.07      | 0.14±0.02    | 499.3±9.87            | 99.41±0.01     |

In vitro Drug Release Studies:

The floating sustained release layer of Dothiepin HCL tablet were designed using individual HPMC K4M, xanthan gum, guar gum, locust bean gum and karaya gum alone and also in combination of two polymers (3:1 HPMC K4M: Natural polymer) and three polymers (3:0.5:0.5 HPMC K4M: Natural polymer 1: Natural polymer 2). The total weight of the polymers in the
formulation used was 33.33% of total weight of SR layer. All the batches of formulated layers were produced under similar condition to avoid processing variables. The in vitro release study of Dothiepin HCL study was conducted in 0.1N HCl for 12 hours. The in vitro release data of Dothiepin HCL is shown in Table 5 and illustrated in Figure 9, 10 and 11. The in vitro release is depending upon nature of drug, nature of polymer, drug to polymer ratio and the medium used. In the present work, HPMC K4M, xanthan gum, guar gum, locust bean gum and karaya gum were used as hydrophilic polymers in the preparation of sustained release layer. The highest release for 12 hrs was observed with formulation F10 which contains HPMC K4M which is commonly used hydrophilic matrix, gets swelled and forming viscous gel thereby rapidly releasing the drug. Among all the formulations, formulation F10 contained 25% HPMC K4M and 4.16% of xanthan gum and guar gum each released 99.75% of drug up to 12 hrs.

Table 5: Percentage cumulative drug released of formulations F1-F15.

| Time  | F1     | F2     | F3     | F4     | F5     | F6     | F7     | F8     |
|-------|--------|--------|--------|--------|--------|--------|--------|--------|
| 5min. | 14.8   | 13.2   | 15.4   | 14.9   | 15.0   | 12.0   | 16.5   | 12.0   |
| 15min.| 28.1   | 29.89  | 29.8   | 30.1   | 30.1   | 33.1   | 34.6   | 31.6   |
| 1hr.  | 49.1   | 50.6   | 50.2   | 51.3   | 50.1   | 43.9   | 51.4   | 55.8   |
| 2hr.  | 53.6   | 54.6   | 54.4   | 55.4   | 54.5   | 51.5   | 60.6   | 60.6   |
| 3hr.  | 62.1   | 63.2   | 60.1   | 61.1   | 63.7   | 62.2   | 63.6   | 68.2   |
| 4hr.  | 66.6   | 71.3   | 63.2   | 64.1   | 67.7   | 66.8   | 71.2   | 77.3   |
| 5hr.  | 77.1   | 80.6   | 74.2   | 76.3   | 77.8   | 74.3   | 75.8   | 80.3   |
| 6hr.  | 84.1   | 91.7   | 83.1   | 81.2   | 85.8   | 77.5   | 86.4   | 87.9   |
| 7hr.  | 87.6   | 96.0   | 88.4   | 92.3   | 88.9   | 80.2   | 88.9   | 90.9   |
| 8hr.  | 97.6   | 98     | 98.4   | 94.5   | 96.5   | 81.6   | 93.4   | 94.8   |
| 9hr.  | 98.1   | –      | –      | –      | 98.5   | 98.9   | 89.7   | 97.0   |
| 10hr. | –      | –      | –      | –      | –      | –      | 89.5   | 98.5   |
| 11hr. | –      | –      | –      | –      | –      | –      | 89.7   | 98.6   |
| 12hr. | –      | –      | –      | –      | –      | –      | 90.9   | –      |

1hr.   | 64.1   | 48.6   | 47.9   | 50.9   | 45.4   | 51.4   | 51.4   | 51.6   |
2hr.   | 64.7   | 53.5   | 58.5   | 61.6   | 53.0   | 60.6   | 62.1   | 62.1   |
3hr.   | 72.2   | 60.8   | 62.1   | 63.6   | 66.6   | 72.5   | 69.7   | 69.7   |
4hr.   | 77.4   | 66.6   | 69.3   | 77.3   | 69.7   | 74.6   | 77.3   | 77.3   |
5hr.   | 81.3   | 71.8   | 74.8   | 82.7   | 75.8   | 83.4   | 81.8   | 81.8   |
6hr.   | 85.9   | 76.3   | 80.6   | 86.7   | 84.8   | 89.4   | 84.9   | 84.9   |
7hr.   | 87.4   | 81.2   | 80.7   | 92.4   | 87.9   | 90.4   | 93.9   | 93.9   |
8hr.   | 88.9   | 85.6   | 83.4   | 95.5   | 89.4   | 91.6   | 95.5   | 95.5   |
9hr.   | 91.9   | 91.6   | 86.3   | 95.5   | 90.9   | 94.0   | 97.0   | 97.0   |
10hr.  | 95.5   | 96.7   | 87.8   | 98.7   | 92.5   | 95.5   | 98.5   | 98.5   |
11hr.  | 98.4   | 97.3   | 89.7   | –      | 95.5   | 99.4   | –      | –      |
12hr.  | –      | 99.7   | 97.0   | –      | 97.0   | –      | –      | –      |
Figure 9: *In-Vitro* release Profile of F-1 to F-5 Formulations prepared with individual polymers.

Figure 10: *In-Vitro* release Profile of F-5 to F-9 Formulations prepared with combination of two polymers.
Figure 11: In-Vitro release Profile of F-10 to F-15 Formulations prepared with combination three polymers.

Release Kinetics:
The in vitro release data from Dothiepin HCL was processed to plot different kinetics approaches. The kinetics of in vitro drug release from the entire formulated bilayer layer tablet obeyed Higuchi release with the high regression $r^2$ value of 0.99 as compared to others. As the polymers used were matrix material hence Higuchi model was applied which showed good linearity with high regression 0.99 suggested that the release mechanism was diffusion controlled. The in vitro release data was subjected to Korsmeyer-Peppas model, which shows good linearity with high $r^2$ value of 0.997 to 0.961. Korsmeyer and Peppas equation superposes two apparently independent mechanisms of drug transport, Fick’s diffusion, and a case-II transport, for the description of drug release from a swelling polymer. For a matrix tablet, when $n$ takes the value of 0.45 it indicates diffusion-controlled drug release and for the value 0.89, it indicates swelling-controlled drug release. Values of $n$ between 0.45 and 0.89 can be regarded as an indicator for both the phenomena (anomalous transport). The $n$ value of optimized formulation F10 is 0.309 and it is clear that all formulation have $n$ values below 0.45. This indicates that the drug release majorly depends on diffusion-controlled phenomenon (Figure 12).
Zero order kinetics

First order kinetics

Higuchi plot

%CDR vs. time

y = 4.764x + 46.196
R² = 0.9892

y = -0.1575x + 2.1408
R² = 0.8051

y = 22.01x + 23.514
R² = 0.9905
CONCLUSION:

Dothiepin HCL floating tablets were developed using one synthetic polymer and four natural polymers in order to achieve sustained release of drug. To develop sustained release layer the polymers were used individually and also in combination. Among all formulation F10 containing HPMC K4M, xanthan gum and guar gum (3:0.5:0.5) released almost all amount of incorporated drug during the period of 12 hrs. This optimized formulation was observed to float in the dissolution media more than 12 hrs. Hence, combination of HPMC K4M with natural polymers Xanthan gum and guar gum can be successfully used to develop floating sustained release tablets.

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