Evidence-Based PET for Neurological Diseases

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13.1 Introduction

Over the past two decades, one of the major breakthroughs for the approach to neurological diseases both in the clinical and research settings has been represented by the validation of diagnostic biomarkers able to demonstrate the presence of pathological mechanisms, alteration in neurotransmission as well as to predict disease progression [1, 2]. The use of PET with different tracers as well as other imaging biomarkers support the etiological diagnosis of neurological disorders in vivo. This approach is particularly relevant in the field of neurodegenerative diseases. In fact, neurodegenerative diseases are characterized by the progressive degeneration and death of neurons. They represent a heterogeneous group of conditions characterized by different etiologies, different neuropathological and neurochemical alterations leading to different clinical pictures and courses [3]. Indeed, an early accurate diagnosis allows to tackle the disease with available or experimental intervention, lifestyle changes, or logistical arrangements, before disability has developed. Early intervention is expected to have greater clinical impact, extend independent and active life, improve its quality, and decrease the burden and costs of the disease [4]. However, the validation of PET tracers in neurological disease is still ongoing, and evidence on its comparative and combined diagnostic value with respect to other biomarkers is incomplete [4, 5]. As a matter of fact, the increasing pressure for cost-effectiveness requires systematic assessment and validation of all biomarker performance in the clinical settings. Similarly only an evidence-based approach to new PET tracers can allow to select the most promising tracers for PET imaging in the research field both for pathophysiological investigations and for upcoming diagnostic approaches.

13.2 Evidence-Based PET in Neurodegenerative Dementia

Although the use of PET tracers for neurotransmission is also actively investigated, the vast majority of PET tracers recently developed for the clinical and pathophysiological evaluation of neurodegenerative dementia aim to evaluate the presence of specific pathological proteins deposition or mechanisms underlying neurodegeneration [3]. Tracers targeting neuroinflammation are also under investigation in this field but their use is still very far from the clinical
Alzheimer’s disease (AD) is by far the most relevant target for brain PET clinical imaging in neurodegenerative diseases [5]. The 2011 World Alzheimer Report has underlined that only a relatively small percentage of dementia cases (ranging between 20 and 50%) are identified and correctly diagnosed in the early stages. This evidence means that at least half of the population of dementia patients does not receive a complete diagnostic workup at disease onset. This diagnostic delay gives rise to a so-called “treatment gap” between early stages of the disease and formal diagnosis, thus delaying correct care and preventing organized support which ameliorates patient’s quality of life (and positively impacting also on caregivers and family members). In the field of AD, two main categories of biomarkers have been proposed to identify the prodromal stage of disease [2, 7]. On the one side, amyloidosis biomarkers are able to identify the molecular/neuropathological feature of AD and include cerebrospinal fluid (CSF) amyloid-β1-42 reduction and brain amyloid accumulation as imaged through PET technology using radiopharmaceuticals that selectively bind to the fibrillar aggregates of amyloid-β plaques (AMY-PET) [2]. On the other side, neurodegeneration biomarkers reflect neuronal injury and downstream neurodegeneration, which can be measured by the increase of tau protein in the CSF, regional atrophy on MRI or synaptic metabolic dysfunction on fluorine-18 fluorodeoxyglucose PET (18F-FDG PET) [2]. As a matter of fact, the progressive dysfunction and loss of neurons lead to distinct involvement of functional systems and major clinical symptoms are mainly determined by the anatomical regions showing neuronal and synaptic dysfunction (which however do not necessarily reflect the molecular changes in the background) [8]. In this framework, MRI has both an exclusionary and inclusionary role for the early assessment of MCI. In fact on one side it can exclude secondary etiology of cognitive symptoms (i.e., vascular damage or normal pressure hydrocephalus) and it can increase the likelihood of a neurodegenerative dementia by highlighting the presence of atrophy in specific cortical regions [9]. Similarly, 18F-FDG PET is a well-founded method for evaluation of brain function and it is useful for the early diagnosis of AD and other dementias in people with mild cognitive impairment (MCI). 18F-FDG PET is a sensitive and specific imaging modality available to support the etiological diagnosis of the underlying neurodegenerative dementia in demented patients. In particular, hypometabolism in the temporoparietal lobe, assessed by qualitative visual interpretation of the scans, represents the typical pattern found in AD [10]. However, despite its widespread use and the well-established role in the clinical settings, the quality of the available studies and thus the role of 18F-FDG PET in identifying patients affected by AD who are still at the stage of MCI are less validated. As a matter of fact, discriminating between patients who will and will not progress to dementia due to AD is critical in the context of care and it must be pursued before patients have crossed the threshold into dementia. One of the background reasons associated with this surprising lack of evidence is related to evolving definition of MCI in the last decade. Unfortunately, the characteristics of the MCI patients recruited in the available published studies are quite diverse across the literature of the last 10 years and this heterogeneity is largely reflected but the lack of a reproducible value of sensitivity and specificity of 18F-FDG PET for the identification of MCI due to AD. Moreover, the sensitivity and specificity of 18F-FDG PET (as well as of all AD biomarkers) depend largely on the method of interpretation. It is, nowadays, advisable to use a combination of visual qualitative and semiquantitative analysis. In fact, the actual general sensitivity and specificity values, although still variable, are higher than 80% for both in the centers where it is utilized computer aided visual read approach such as Statistical Parametric Mapping (SPM), three-dimensional Stereotactic Surface Projection (3-D-SSP) statistics (Neurostat) or AD t-sum implemented in other software [11, 12]. Software able to combine information from MRI and 18F-FDG PET (even in the multicenter settings) have also been developed and have been demonstrated to
improve detection and differentiation of AD and FTD (with 88–100% accuracy for AD detection) [13].

In more recent years, the availability of PET biomarkers of amyloid deposition such as $^{11}$C-PiB and $^{18}$F-labeled tracers ($^{18}$F-Flutemetamol, $^{18}$F-Florbetaben, and $^{18}$F-Florbetapir) has gained great attention [14]. These tracers exhibit high affinity binding for fibrillary amyloid that is a hallmark of AD and can be found in moderate to high number in cortical gray matter in all cases of AD developing many years before the onset of dementia. The vast majority of preliminary studies with amyloid PET has been carried out with $^{11}$C-PiB. It has been reported by measuring $^{11}$C-PiB distribution in MCI and control subjects, that MCI patients who converted to AD, at an estimated rate of 25% per year, had greater $^{11}$C-PiB retention in several brain area with a 93.5% sensitivity and 56% specificity [15]. Moreover, none of the $^{11}$C-PiB negative MCI patients demonstrated to be converted to AD indicating that $^{11}$C-PiB negativity had a 100% negative predictive value for progression to AD [7, 16]. However, due to the 20-min half-life of $^{11}$C, $^{11}$C-PiB can only be used in PET centers with on-site cyclotron and radiopharmacy facilities while $^{18}$F is a more suitable radioisotope for widespread clinical use. Accordingly, the availability of fluorinated amyloid PET tracers has favored a greater impact of this tool also in the clinical settings [17]. In particular, a sensitivity of amyloid $^{18}$F-labeled tracers ranging from 89 to 97%, with a specificity ranging from 63 to 93% has been reported both for visual and semiquantitative analysis and no significant differences have been highlighted among the different agents [18].

The overall impacts of AMY-PET from the reported literature are a change of diagnosis and management in 35.2% and 59.6% of cases, respectively, leading to reduction in unnecessary investigations, treatments, relief of distress of caregivers, and potential involvement in clinical trials [19].

In particular, AMY-PET (as well as CSF data) are relevant for the differential diagnosis of etiologies underlying primary progressive aphasia (PPA). In fact, it has been suggested that the current clinical classification system for PPA should aim to predict underlying pathology across different cohorts and clinical settings which has a greater specificity with respect to neurodegeneration biomarkers (MRI and $^{18}$F-FDG PET) [20]. In fact, although patients’ characteristics including age and ApoE genotype should be considered when interpreting AMY-PET, it has been highlighted that AMY-PET positivity is significantly more prevalent in logopenic variant of PPA, which belongs to the AD spectrum, (86%) than in non-fluent variant of PPA (20%) or semantic variant of PPA (16%) which should be part of the spectrum of fronto-temporal degeneration [21]. It should be noted however that cognitive normal older people has a high burden of amyloid defined as incidental amyloidosis. Indeed, the presence of amyloid deposition is not sufficient to define the presence of pathophysiological processes associated with AD which has to include the concomitant tau deposition [22]. Analyses in AMY-PET positive cognitive normal subjects have shown that the episodic memory and global cognitive function consistently had the largest, albeit still modest, effect sizes between performance and amyloid burden, whereas executive function, working memory, processing speed, visuospatial function, and semantic memory exhibited relatively smaller effect sizes [23]. Moreover, the incidence of brain amyloidosis increases with aging in all non-AD populations and has been repeatedly reported in other neurological conditions such as in dementia with Lewy bodies (DLB) and Parkinson’s disease (PD). Similarly, all amyloid PET tracers have affinity to amyloid in vessel walls, and can thus result in positive scans in case of cerebral amyloid angiopathy (CAA) [7]. In this framework, it has been demonstrated that the ratio between the occipital and the whole brain uptake is higher in patients with CAA than in patients with AD, possibly suggesting a more limited regional amyloid deposition on CAA [24]. Accordingly, AMY-PET has a moderate to good diagnostic accuracy for the identification of patients with CAA; especially as a negative scan it is useful to rule out CAA in the appropriate clinical setting [25]. Finally, it should be noted
that soluble Aβ oligomers and neurofibrillary tangles (NFTs), the other histopathologic cores of Alzheimer’s disease are not detected by this method, possibly producing false negative results [26].

## 13.3 Evidence-Based PET for Movement Disorders

Movement disorders are a group of neurologic syndromes characterized by an excess of movement or a scarcity of voluntary and automatic movements [27] related to different neurodegenerative or acquired central nervous system diseases affecting structures involved in movement control and modulation such as basal ganglia, cerebellum, cortex, and different thalamic nuclei. Parkinson’s disease (PD) represents the second most common neurodegenerative disorder after AD and is typically characterized by motor and non-motor manifestations. Motor dysfunctions include bradykinesia, resting tremor, and muscular rigidity [28] as the result of dopaminergic deficit due to degeneration of the dopaminergic nigrostriatal system [29]. On the other hand, non-motor features usually associated with the damage in non-dopaminergic pathways may include depression, olfactory and autonomic dysfunction, sleep disorders, psychiatric symptoms, pain, fatigue, and cognitive impairment [30] and can, in some case, even precede the motor phase by several years [31]. Besides the most prevalent PD, there are other related atypical parkinsonian syndromes (APS) also known as Parkinson-plus syndromes. From the neuropathological point of view, on the basis of the predominant multisystemic progressive accumulation of misfolded proteins, parkinsonian disorders could be classified into α synucleinopathies (PD with and without cognitive impairment/dementia, dementia with Lewy bodies—DLB, and multiple system atrophy—MSA) and tauopathies (corticobasal degeneration—CBD and progressive supranuclear palsy—PSP). All the aforementioned conditions must be distinguished from non-degenerative causes of parkinsonism (e.g., toxic/drug-induced, psychogenic, or vascular etiologies) in which presynaptic nigrostriatal pathways are preserved. Molecular imaging has proven to be a powerful tool for improving our understanding of the pathophysiology underlying parkinsonian disorders. In particular, PET and single photon emission computed tomography (SPECT) imaging are used as surrogate of unique in vivo functional measurement of monoaminergic pathways impairment in neurodegenerative diseases since the early 1980s [32]. Actually, these techniques are able to evaluate and detect nigrostriatal degeneration from different points of view. The analogue of levodopa 18F-fluorodopa (18F-DOPA) is a PET tracer that estimates the activity of aromatic amino acid decarboxylase enzyme (AADC), which converts levodopa into dopamine in striatal cells, thus reflecting dopamine synthesis. After its conversion in 18F-fluorodopamine, it follows the same fate of endogenous dopamine and is thus transported to intraneuronal storage vesicles by vesicular monoamine transporter 2 (VMAT2) [33] to then be released into the synaptic cleft and interact with postsynaptic dopamine receptors.

On the other hand, presynaptic dopamine transporter (DAT) density, responsible for reuptake of dopamine (DA) from the synaptic cleft and typically reduced in PD [34], can be measured through 123I-FP-CIT (123I-ioflupane), one of the most used radiotracers for SPECT imaging, or with specific PET tracers (18F-PE2I; N-(3-iodoprop-2Eenyl)-2β-carbomethoxy-3β-(4-methyl-phenyl)nortropane). Finally, specific radiolabeled ligands for VMAT2 also exist and can be used in PET imaging for research purposes (11C- and 18F-dihydrotetabenazine). The applicability of functional imaging in the evaluation of striatal dopaminergic degeneration in control subjects and PD patients is well documented. Actually, PET and SPECT studies with AADC, VMAT2, and DAT tracers are able to monitor nigrostriatal deficit over time demonstrating the negative effects of age on DA transporters and receptors. According to Karrer et al. [35], age has a significantly larger effect on D1- than D2-like receptors with an average age reduction across the DA system of about 3.7–14.0% per decade. On the contrary, DA synthesis capacity seems to
be spared from this detrimental effect. This finding nicely fit with the results of a contemporary meta-analysis of Kaasinen et al. [36] including PD patients submitted to PET and SPECT studies for the evaluation of striatal presynaptic dopamine function. In this meta-analysis, it was demonstrated a higher defect in DAT and VMAT2 function compared to AADC defect in PD patients. This difference is possibly due to the effect of a compensatory upregulation in AADC function, confirming vesicular monoamine transporter 2 and dopamine transporter as the most sensitive targets to assess. In the same study, a linear correlation between disease severity and dopamine loss was demonstrated and a mean motor disease duration of 4–7 years was needed to overcome the general compensatory changes in the terminal area of the nigrostriatal tract in PD and induce a detectable loss of about 50% of putaminal presynaptic dopamine function. It should be noted, however, that 18F-DOPA PET is a valid alternative to 123I-FP-CIT SPECT. Similarly, PET VMAT2 tracers as 11C- and 18F-labeled dihydrotetrabenazine are very sensitive in detecting presynaptic dysfunction in PD without significant influence by compensatory changes [37] but are less available than other tracers. Besides dopaminergic dysfunction, serotonergic system exerts an important role in PD pathophysiology. Among PET ligands that have been developed for the evaluation of serotonergic receptors and serotonin transporter (SERT), 11C-DASB is a second-generation PET ligand with the best selectivity for the SERT [38]. In their systematic review examining the in vivo SERT changes in PD measured by 11C-DASB PET, Pagano et al. [39] demonstrated that SERT dysfunction is associated with the development of several motor (tremor and dyskinesias) and non-motor symptoms (depression, fatigue, apathy, and weight changes). In particular, they observe a highest decrease in SERT binding in the rostral raphe and caudate followed by putamen, thalamus, ventral striatum, caudal raphe, and hypothalamus, according to succession of pathological events in serotonergic neurons described by Braak’s PD staging [29]. Furthermore, reduced SERT binding in putamen is associated with longer duration of the disease, whereas lower 11C-DASB binding in caudate is associated with worse cognitive function and older age. Interestingly, although SERT binding in putamen decreased with the progression of the disease, PD patients with dyskinesias have relatively preserved putaminal serotonergic function with mechanisms not fully clarified.

Moreover, PET and SPECT are able to detect pathologic changes from the earliest phase of the disease, improving diagnostic accuracy in the early stages [40]. REM sleep behavior disorder (RBD) confirmed by polysomnography is a parasomnia occurring during REM sleep characterized by the loss of physiological muscle atonia and associated with dream-enacted behaviors. It is defined “idiopathic” when appears isolated, without any other clinical sign of a neurological disorder. However, more than 80% of idiopathic RBD patients will develop a definite neurodegenerative disease, mostly a synucleinopathy. Furthermore, the presence of abnormal presynaptic dopaminergic PET or SPECT scan is considered the second most relevant risk factor for prodromal PD [41] predicting a high risk for short-term conversion into a synucleinopathy in idiopathic RBD patients [42]. A recent meta-analysis about the role of presynaptic dopaminergic imaging in RBD shows that idiopathic RBD patients exhibit decreased nigrostriatal dopaminergic functioning in comparison with healthy controls, especially at the putamen level. Furthermore, patients with idiopathic RBD and patients with PD without RBD exhibit a similar degree of nigro-caudate dopaminergic deafferen- tation [43].

Molecular imaging can also facilitate the differential diagnosis among PD, atypical parkinsonian syndromes (APS), essential tremors, and other degenerative conditions that represent a group of complex and heterogeneous diseases with overlapping symptomatology and variable response to dopaminergic medications. 123I-FP-CIT SPECT can distinguish degenerative forms of parkinsonism from essential tremor [44], drug-induced Parkinsonism [45] and could also differentiate DLB from AD. Subjects with PD and APS show indeed an early reduction of striatal
dopaminergic binding [46] usually before the appearance of motor symptoms. On the contrary, patients with essential tremor, drug-induced parkinsonism, and AD are characterized by normal dopamine transporter uptake [47]. Although a differential pattern has been described at the group level, a real distinction between the various degenerative forms of parkinsonism is not possible by means of SPECT assessment only. To this purpose, \(^{18}\text{F}-\text{FDG}\) PET has demonstrated to be more promising. As suggested by Albrecht et al. [48], glucose hypometabolism at \(^{18}\text{F}-\text{FDG}\) PET can identify consistent functional brain abnormalities in PD, outperforming structural MRI. In particular, while MRI showed only focal and inconsistent alterations, in PD patients the authors found an extensive glucose hypometabolism in bilateral inferior parietal cortex and left caudate nucleus that is related to cognitive deficits (inferior parietal cortex) and motor symptoms (caudate nucleus). Disease-specific patterns of regional glucose metabolism in patients with parkinsonism are well documented [49, 50]. However, the valuable capability of \(^{18}\text{F}-\text{FDG}\) PET for accurate differentiation between PD and APS has been unanimously accepted only in recent years. In a preliminary meta-analysis, Meyer et al. well described the different \(^{18}\text{F}-\text{FDG}\) uptake pattern in PD and APS [51]. PD is characterized by a posterior temporoparietal, occipital, and sometimes frontal hypometabolism with a relative hypermetabolism of the putamen, pallidum, thalamus sensorimotor cortex, pons, and cerebellum.

MSA patients show instead a marked hypometabolism of the putamen (mainly in its posterior portion), pons, and cerebellum, which may be more pronounced in the striatum or in the pons and cerebellum, on the basis of the clinical presentation. Conversely, PSP is characterized by a regional hypometabolism preferentially involving the medial, dorsal, and ventrolateral frontal areas (i.e., the anterior cingulate gyrus, supplementary motor area, precentral gyrus, and premotor-to-posterior prefrontal areas); caudate, thalamus, and upper brain stem. Finally, CBD patients have a typically highly asymmetric hypometabolism of the frontoparietal areas, striatum, and thalamus contralateral to the most affected body side. A concomitant cortical hypometabolism may be mainly found in the parietal cortex and usually extends across the sensorimotor cortex into the cingulate gyrus and premotor-to-posterior prefrontal areas.

\(^{18}\text{F}-\text{FDG}\) PET has proved to be particularly relevant also for the diagnosis of DLB and is actually listed among the supportive biomarkers for its identification [52]. DLB is characterized by a more prominent hypometabolism affecting the primary visual cortex and occipital cortex with relative preservation of subcortical structures and primary somatomotor cortex and with a concomitant hypometabolism in posterior associative cortex. In particular, the presence of a hypometabolism in the precuneus with a relative sparing of glucose uptake in posterior cingulate gyrus is known as “cingulate island sign” and has proved to significantly increase \(^{18}\text{F}-\text{FDG}\) PET specificity for the differential diagnosis with respect to AD, although lower than DAT SPECT [53].

\(^{18}\text{F}-\text{FDG}\) PET evidence is also available for Huntington’s disease gene expression carriers (HDGECs). Actually, several PET imaging studies investigating the glucose metabolism in HDGECs have shown specific metabolic patterns mainly characterized by a progressive reduction of subcortical and cortical glucose metabolism in the striatum, thalamus, insula, posterior cingulate gyrus, and prefrontal and occipital cortex associated to a relative hypermetabolism in the cerebellum and pons [54]. In particular, reduction in striatal metabolism seems to be an early feature of the disease, preceding neuronal loss and thus motor onset of the disease. However, glucose metabolism deficits are only one of the many factors involved in Huntington’s disease and \(^{18}\text{F}-\text{FDG}\) PET is not indicated for the diagnosis of this disease. Besides \(^{18}\text{F}-\text{FDG}\), other striatal PET radioligands have been used in this context. In particular, a meta-analysis aiming to investigate striatal molecular changes in 158 premanifest and 191 manifest HDGECs patients [10] demonstrates a significant decrease not only in glucose metabolism in caudate and putamen but also in dopamine D2 receptors and in striatal phosphodiesterase 10A binding. This findings well reflect the different
and depressive pseudodementia, in the specific field of psychiatric disorders, PET technology has more extensively been used for research purposes to determine pathophysiology of diseases and response to intervention [59]. In particular, the availability of tracers for imaging of neurotransmission allows the investigation of different systems (i.e., serotonin, dopamine GABA pathways) and to investigate a wide range of psychiatric diseases. Similarly, brain PET with different tracers (i.e., tracers for neuroinflammation) has been used to explore new hypotheses related to the onset of psychiatric diseases. The vast majority of PET studies carried out in the last 20 years in psychiatric patients have aimed to map functional alterations and mechanism underlying major depressive disorder (MDD), a common mental illness with high lifetime prevalence (close to 20%). Indeed, although the presence of aberrant brain activation during cognitive and emotional processing has been extensively evaluated in MDD patients, results of available studies vary considerably. Muller and colleagues summarized the evidence derived from neuroimaging experiments (using fMRI or PET) of group comparisons between adults with unipolar depression and healthy controls, reporting significant activation differences between patients and controls during emotional or cognitive tasks [60]. Several inconsistencies across available studies emerged from this systematic review. Brain metabolism in MDD was also specifically addressed in several voxel-based PET studies which were submitted to a meta-analytical approach by Su et al. [61]. Again while decreased prefrontal, insular, and limbic cerebral glucose metabolism was repeatedly highlighted in depressed patients with respect to healthy controls, available literature has not always been consistent. In this framework, the involvement of specific regions such as insula, limbic system, basal ganglia, thalamus, and cerebellum was more frequently reported, suggesting that these regions are likely to play a key role in the pathophysiology of depression. In keeping with these results, convergent change in the limbic-cortical brain circuit in depression compared to controls was also found in multi-modal imaging studies involving both PET and MRI data. Reported
specific changes include lower gray matter volumes in amygdala, dorsal frontomedian cortex, and the right paracingulate cortex, as well as relative hypermetabolism in the right subgenual and pregenual anterior cingulate cortices. Building a strong and evidence-based mapping of these alterations in MDD is relevant as these regions could serve as a specific region-of-interest-disease template for both in vivo imaging in individual patients and postmortem histopathologic exploration [62]. Other PET studies investigated altered function related to different pathways including 5-HT receptor and transporter dysfunction in neuropsychiatric disorders. Indeed, impairment of serotonin receptor and transporter function is increasingly recognized to play a major role in the pathophysiology of neuropsychiatric diseases including anxiety disorder, major depressive disorder, bipolar disorder, and schizophrenia. In particular, a retrospective analysis revealed that these psychiatric disorders differed in affected brain regions, affected synaptic constituents as well as direction of dysfunction in terms of either sensitization or desensitization of transporter and receptor binding sites [63].

Striatal presynaptic dopamine pathway has been the most frequent target for PET and SPECT imaging in schizophrenia [64]. As a matter of fact, the role of striatal dopaminergic neurotransmission in the onset of symptoms of schizophrenia (including psychotic symptoms) is currently targeted by dopaminergic drugs. A specific marker of the integrity of presynaptic dopamine neurons in the striatum, the density of striatal dopamine terminals, can be quantified through molecular neuroimaging of DAT. A meta-analysis of DAT density in the striatum of schizophrenic patients demonstrated that striatal DAT density was not significantly different between patients and controls [64]. Similar negative findings were regionally confirmed in putamen and caudate. There was no moderating effect for external factors such as antipsychotic medication or illness duration. Accordingly, the authors concluded that loss of integrity of striatal dopaminergic synapses is not critical for the emergence of schizophrenia and these findings are relevant for further refining dopaminergic hypotheses of schizophrenia (with possible repercussion on interventional studies aiming to identify new treatment options). By contrast, a different window on presynaptic dopaminergic function was opened by studies exploring this pathway through $^{11}$C-$^{18}$F-DOPA PET [65]. Available studies were summarized in the meta-analysis by Fusar-Poli and Meyer-Lindenberg [65]: patients with schizophrenia showed increased striatal uptake as compared with controls and this finding was regionally confirmed in both caudate and putamen. Finally, no significant effect of age, illness duration, gender, psychotic symptoms, and exposure to antipsychotics was highlighted.

PET and SPECT studies with several tracers have been used on other neuropsychiatric diseases including obsessive compulsive disorders, Tourette’s syndrome (TS), and attention deficit hyperactivity disorder (ADHD) as well as to test brain function in specific conditions such as in case of ecstasy/polydrug use and disorders of consciousness. In particular, dopaminergic imaging with PET and SPECT was able to demonstrate dopaminergic alterations in TS and pathophysiology and psychostimulant treatment of attention deficit in ADHD. In fact, dopaminergic alterations in TS are in line with the current pathophysiological hypotheses of a tonic-phasic dysfunction in the dopamine system although available studies are characterized by low effect sizes due to the heterogeneity of the disease [67]. Similarly, although dopaminergic studies in ADHD yielded inconsistent results often demonstrating either high and low striatal dopamine transporter levels across different studies, a systematic review of the available evidence highlighted that striatal dopamine transporter density in ADHD is depended on previous psychostimulant exposure, with lower density in drug-naive subjects and higher density in previously medicated patients [68]. More general approaches on brain perfusion and metabolism by means of SPECT and PET allowed to demonstrate that
pharmacological and psychological treatments reduce resting cortico-striato-thalamo-cortical circuit activity in obsessive compulsive disorder. Similarly markedly reduced activity within midline cortical and subcortical sites (anatomical structures linked to the default-mode network) are present in patients with disorders of consciousness [69, 70]. Finally, PET studies on post-synaptic 5HT2A receptor imaging allowed to highlight that serotonin axons with the longest projections from the raphe nuclei might be more markedly affected by ecstasy/MDMA use.

13.5 Conclusions

In conclusion, a huge body of literature has highlighted an ongoing and promising role of PET with different tracers in neurodegenerative dementia, movement and psychiatric disorders. In some clinical settings such as in case patients with mild cognitive impairment and dementia, for the differential diagnosis of underlying etiology as well as for the early and accurate identification of patients with neurodegenerative parkinsonian syndromes, PET has gained an increasing relevant clinical role. By contrast the possibility to accurately quantify neurotransmission with different tracers is increasingly supporting the use of PET technology for pathophysiological and interventional studies in patients with psychiatric disorders. In both cases (clinical use of PET in neurodegenerative dementia and parkinsonian syndromes and research use of PET in psychiatric disorders), it is crucial to proceed with robust methodology which starts with the systematic evaluation of evidence-based results of previous studies. Only this approach will allow to balance costs and clinical advancement, thus meeting the needs of both patients and health-care systems.

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