Photocracking Silica: Tuning the Plasmonic Photothermal Degradation of Mesoporous Silica Encapsulating Gold Nanoparticles for Cargo Release

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Abstract: The degradation of bionanomaterials is essential for medical applications of nanoformulations, but most inorganic-based delivery agents do not biodegrade at controllable rates. In this contribution, we describe the controllable plasmonic photocracking of gold@silica nanoparticles by tuning the power and wavelength of the laser irradiation, or by tuning the size of the encapsulated gold cores. Particles were literally broken to pieces or dissolved from the inside out upon laser excitation of the plasmonic cores. The photothermal cracking of silica, probably analogous to thermal fracturing in glass, was then harnessed to release cargo molecules from gold@silica@polycaprolactone nanovectors. This unique and controllable plasmonic photodegradation has implications for nanomedicine, photopatterning, and sensing applications.

Keywords: degradation; plasmonic; gold nanoparticles; mesoporous silica nanoparticles; photothermal; polymer coating

1. Introduction

Engineering bioinorganic nanomaterials with controllable degradability rates is essential to prevent toxic bioaccumulation into the body after their diagnostic or therapeutic intended purposes [1–4]. Among bioinorganic nanomaterials [5], mesoporous silica and organosilica nanoparticles (NPs) are promising hybrid nanomaterials for biomedical applications [6,7]. Silica particles have indeed many unique benefits such as tunable dissolution rates from under a day to months [1], high surface areas and pore volumes (e.g., 1000–1500 m²·g⁻¹; 1.0–4.5 cm³·g⁻¹) [8,9], and can be produced in kilogram quantities while maintaining a high control of particle monodispersity [10]. Silica can be hybridized using organic and inorganic doping strategies to mediate biodegradability through pH [11,12], enzymatic [12–14], redox [3,15–18], and biochelation [19–22] mechanisms [1,2]. The controlled silicon chemistry and hybridization of silica NPs also enables controlled surface modifications for various applications [6,23–28] including drug delivery [6,29–32] and medical diagnosis [33–35].

Plasmonic NPs are increasingly used as photothermal (PT) transducers for a wide variety of applications in colloidal and surface sciences [36–43]. The control of the PT efficacy of various metal NPs has numerous potential applications as witnessed by the increasing number of theoretical and experimental studies [36–38,44–50]. Detailed studies of the PT efficacies of gold NPs revealed high-energy bleaching of NIR resonant bands for gold shells and rods (the relative PT efficacy decreased by 16–22 times), which was not observed for gold spheres [51]. Gold nanospheres are transducers that
can produce very high local temperatures. Plasmonic NPs are often embedded within various shells or matrices for biomedical applications using the PT effects. Gold NPs are typically coated with polymers (e.g., polyethylene glycol) to maintain long circulation times in the bloodstream and promote their accumulation into cancer cells [52]. In addition, neutral polymers, liposomes [53], polyelectrolytes [54], and mesoporous silica shells have been coated onto gold NPs to combine the loading properties of the coating matrices with the PT features of the plasmonic cores [55]. Regarding the PT degradation is silica, one hundred nanometer-large silica particles encapsulated inside an 18 nm-thick gold shell were dissolved by a powerful near-infrared (NIR) femtosecond pulsed irradiation (90 fs pulses; 1 kHz; 1 ml/pulse; total energy of 180 µJ) [56]. The PT effect even disrupted gold shells at higher power (300 µJ) [56]. Croissant and Zink also discovered that silica could be dissolved upon PT actuation at low power [57]. Taken together, these studies have demonstrated that PT effects can be used to photodegrade silica-based nanomaterials, however, the parameters governing the photodegradation have not been identified and doing so would allow the control of biodegradability rates for safe and effective biomedical applications.

Herein, we report the surprisingly powerful PT silica cracking in Au@MSN by tuning the size of gold nanocores, or the power and wavelength of the laser irradiation in the visible region (Figure 1). To demonstrate these features, we designed two types of Au@MSN, one containing monodisperse 15 nm-wide gold nanocores, and another encapsulating polydisperse gold NPs of sizes ranging from 5–40 nm. On the one hand, Au@MSN containing monodisperse gold cores were used to study the influence of the laser power on the photocracking. On the other hand, Au@MSN containing polydisperse gold cores were used to demonstrate the influence of the gold diameter and laser wavelength on the silica photodegradation. Finally, the usefulness of the tunable PT degradation of silica was highlighted using Au@MSN@Polycaprolactone (PCL) nanovectors to release cargo molecules upon laser excitation. This unique and controllable plasmonic photodegradation has implications for nanomedicine, photopatterning, and sensing applications.

Figure 1. Photodegradation of mesoporous silica nanoparticles encapsulating gold nanocores is dependent on the size of the gold cores and the wavelength of the irradiation.

2. Results and Discussion

In view of monitoring the effect of the laser power on the silica photocracking independently of the gold nanoparticle diameter (which impacts the photothermal efficiency [58]), we first prepared
Au@MSN nanomaterials displayed a narrow size distribution centered at 150 nm, had a surface area of about 870 m$^2$·g$^{-1}$, and average pore sizes of 2.2 nm (Figures S1 and S2). The mesoporous silica shell had an average thickness of 69 ± 10 nm (Figure S3, see Supplementary Materials).

The plasmonic photodegradation of silica was first investigated by monitoring the integrity of the mesoporous silica framework stability before and after irradiation Au@MSN samples via transmission electron microscopy (TEM). The experiments were carried out by directing a laser beam on nanoparticle powders (~2 mg) placed at the bottom of quartz cuvettes filled with deionized water (~2 mL) [57]. The remarkable silica photodegradation is shown by TEM micrographs before and after 7 h of irradiation (514 nm, 50 mW) of Au@MSN (Figure 2A,B respectively). The qualitative comparison in Figure 2C shows the increasing photodegradation of silica (different particles are compared after the same irradiation time). The PT conversion evolution (Figure 2C) is the result of the experimental fact that all the NPs are not receiving the same treatment under the irradiation geometry used (see Materials and Methods Section). The cause of the silica cracking is clearly the PT effect from the gold cores as implied by the inside out degradation patterns. TEM images strongly suggested growing internal holes which eventually lead to the cracking of the particles (Figure 2B,C). Besides, the holes or cracks present within Au@MSN did not always match the spatial position of the gold cores (see Figure 2B,C and Figure 4A at 530 nm) which suggests that that the destruction of silica was not primarily due to the vibration of gold NPs under irradiation, but rather to the PT degradation of the weakest parts of the porous silica framework. Going a step further, we decided to assess the possibility of regulating the plasmonic PT efficacy using various irradiation powers and wavelengths.

![Figure 2](image_url)

**Figure 2.** TEM images of Au@MSN before irradiation (A), and after 7 h of irradiation through an argon ion laser at 514 nm under 50 mW (B). Impact of the PT conversion of the gold cores on the MSN matrix under 50 mW (C).
The influence of the laser power on the silica photodegradation was then evaluated. Au@MSN NPs were irradiated at 514 nm for 14 h under 15 and 100 mW (Figures 3A and 2B respectively). Lower power (15 mW) did not show any photodegradation, whereas TEM images displayed a complete silica photodegradation at higher power (100 mW). Note that bare MSN without gold cores were also irradiated at 514 nm under 100 mW for 14 h in a control experiment, and none of the NPs were damaged (Figure 3C). Importantly, we have already demonstrated plasmonic heating of at least 60 °C inside Au@MSN in identical conditions (15 mW, 514 nm) for cargo release applications [57], which implies that the integrity of the silica framework remains untouched under plasmonic PT effects until the local temperature is sufficiently high [57]. It should also be noted that the bulk temperature of the NPs solution did not significantly change before and after irradiation. Besides, as discussed in following sections, using powers of 20 to 30 mW (for 30 min or 7 h) also lead to silica photocracking (Figures 4, 5 and 6F), while the photodegradation was much more severe for the same duration under 50 mW (Figure 2B,C). These observations confirm the power dependence of plasmonically-actuated silica degradation. Notably, gold NPs did not appear to degrade, unlike other studies using higher powers [56].

![Figure 3. TEM images of Au@MSN irradiated 14 h at 514 nm under 15 mW (A), and 100 mW (B) displaying the power dependency of PT effect. Intact bare mesoporous silica NPs after irradiation for 14 h at 514 nm under 100 mW (C). Scale bars of 100 nm are used (A–C).](image)

To study the influence of the laser wavelength and the diameter of gold cores on the silica photocracking, Au@MSN were prepared with polydisperse gold nanocores. This strategy allowed the rigorous assessment of the role of the size on the photocracking since all gold particles will have the same surface capping agents and will be encapsulated in an identical silica matrix, unlike multiple samples of Au@MSN obtained by different procedures to contain gold NPs of different sizes. Au@MSN with polydisperse gold nanocores (ca. 5–40 nm-wide) were characterized by TEM and DLS and displayed sizes of ca. 150 nm, a surface area of ca. 960 m²·g⁻¹ and average pore sizes of 2.4 nm (Figures S4 and S5). The mesoporous silica shell had an average thickness of 133 ± 14 nm (Figure S6). The polydispersity of gold nanocores was confirmed by the wider plasmon band in the UV–vis spectrum when compared to Au@MSN containing monodisperse 15 nm-wide gold cores (Figure S7). The plasmonic heating was expected to correlate with the extinction coefficients of the gold NPs, which in turn is correlated with the gold particle diameter. Indeed, both the extinction coefficient and the wavelength of maximum extinction increase as the particle size increases, but the extinction coefficient is much more sensitive to the size than to the wavelength. For example, the plasmon band maxima (λmax) and molar extinction coefficients (ɛ) have been reported to be λmax = 524 nm and ɛ = 7 × 10⁷ L·mol⁻¹·cm⁻¹, λmax = 524 nm and ɛ = 78 × 10⁷ L·mol⁻¹·cm⁻¹, and λmax = 530 nm and ɛ = 540 × 10⁷ L·mol⁻¹·cm⁻¹ for 7.5, 16, and 35 nm-wide gold NPs, respectively [58].

To experimentally test this correlation, Au@MSN were initially irradiated at three different wavelengths (448, 530, and 568 nm) under 20 mW for 30 min to study the wavelength-dependence of the photodegradation (Figure 4A). In this experiment, a clear dependence on the irradiation wavelength...
on the mesoporous silica photodegradation was observed, since the silica shell was cracked at 530 nm, while a hollow mesoporous silica nanostructure was generated at 568 nm (Figure S8). However, silica shells were surprisingly intact at 448 nm under the same power (Figure S8). This photodegradation was obtained after a relatively short time of irradiation (30 min), which demonstrated the efficiency of the process previously observed after 14 h of irradiation at 514 nm (Figure 2C). Secondly, irradiations at five different wavelengths were performed on Au@MSN (20 mW; 30 min) and three size ranges (5–10, 15–20, and 25–35 nm) were compared (Figure 4). On the one hand, the 5–10 nm size range showed a slight degradation of the silica matrix at 448 nm (Figure 4A). On the other hand, the 25–35 nm size range did not exhibit silica degradation at these lower wavelengths, but the photocracking and dissolution of silica were observed at higher wavelengths (530 and 568 nm, Figure 4C). The middle 15–20 nm size range displayed the silica photodegradation from 514–568 nm (Figure 4B). Such behavior is consistent with the plasmonic properties of gold nanocrystals of different sizes.

Several unique NPs in our experiments also suggested that gold NPs could be selectively excited by tuning the wavelength of irradiation. Figure 5 shows the unique case of two Au@MSN fused during the sol–gel process which contains two different 15 and 5 nm-wide gold cores sufficiently separated to be considered independent. Astonishingly, the photocracking of silica selectively occurred around the 15 nm-wide core upon irradiation at 514 nm, as predicted by the wavelength and size dependence observed in Figure 4. Note that the reverse situation was found in Figure S8A where 5 and 15 nm-wide gold cores were encapsulated within one silica shell and the 448 nm irradiation revealed a slight local degradation around the 5 nm core, leaving the 15 nm core area intact. These observations strongly suggested that plasmonic particles can be selectively excited to photodegrade materials which open new horizons in selective photolithography or dual cargo release using fused twin core–shell nanosystems containing plasmonic particles of different sizes.
The controlled plasmonic photodegradation of silica particles was finally applied for remote cargo release. Au@MSN nanomaterials with 15 nm cores were loaded with the rhodamine B dye in aqueous solution and then coated with an alkoxysilylated polycaprolactone (PCL, 2000 g·mol\(^{-1}\)) to prevent the dye leakage (Figure 5A and Figure S9A). The alkoxysilylated PCL was obtained from the coupling of the commercial PCL diol with 3-(trimethoxysilyl)propyl isocyanate in toluene (ESI). The successful polymer coating onto Au@MSN was confirmed by TEM before (Figure 6B) and after PCL attachment (Figure 6C,D and Figure S10). This was further validated by Fourier transform infrared (FTIR) spectroscopy displaying the polymeric \(\nu_{\text{C–H}}\) vibrational modes between 2950 and 2850 cm\(^{-1}\) and the \(\nu_{\text{C=O}}\) carbonyl mode at 1692 cm\(^{-1}\) (Figure S9B). A rhodamine B payload of 3 wt % was calculated using UV–visible analysis of the loading supernatant. Then, dye-loaded Au@MSN@polymer were placed at the bottom of a quartz cuvette filled with deionized water and irradiated at 514 nm under 30 mW (Figure 6E). The flat baseline before laser irradiation was characteristic of a robust nanocarrier devoid of premature cargo leakage. When the laser was turned on, however, an instantaneous release of rhodamine B cargos was triggered (Figure 6E). The full release of cargos was reached after nearly 1000 min.

Various analyses and control experiments were eventually performed to understand the mechanism of the cargo release. TEM analyses of the irradiated Au@MSN@polymer nanocarriers revealed that the release of the cargo was due to the photocracking of silica nanoshells (Figure 6F). The selection of PCL coating was also purposeful for its low melting temperature (60 °C) which corresponds to the local heating generated in our nanosystem (30 mW at 514 nm) [57]. A local temperature increase of at least 60 °C within Au@MSN@polymer NPs working in tandem with the photocracking of silica thus accounts for the release of cargos under irradiation. Two control experiments were carried out to confirm (i) the thermo-responsiveness of the coating of Au@MSN@polymer particles and (ii) the loading of cargos into silica pores rather than into the polymer shell. First, cargo-loaded Au@MSN@polymer particles were placed into an oil bath at 60 °C to evaluate the thermo-responsiveness of PCL. Consistent with our expectations, no cargos were released before heating the particles and when the external heating was turned on, the release of cargos occurred (Figure S12). Secondly, solid (non-mesoporous) Stöber silica NPs were synthesized [61] (see TEM images in Figure S11) along with bare mesoporous silica particles [57]. Both particle types were mixed with Rhodamine B cargos overnight and then coated with silylated PCL molecules. Release experiments were then conducted with the oil bath set again at 60 °C (Figure S13). Stöber silica@polymer particles released only 0.01 wt % of cargos whereas MSN@polymer released ca. 2.02 wt % which demonstrated that most cargo molecules were loaded into the pores of silica particles rather than into the polymeric shell. We concluded that these experiments
and characterizations confirmed a release mechanism involving the PT melting of PCL synergistically with the silica photocracking.

![Figure 6](image)

**Figure 6.** Schematic representation of the dye loading and polymer coating of Au@MSN (A). TEM micrographs before (B) and after polymer coating (C, D). Light-triggered cargo release in solution (514 nm, 30 mW) (E). TEM photodegradation of the dye-loaded Au@MSN@polymer nanoparticles after 7 h of release experiment (F).

3. Materials and Methods

**Materials.** Potassium tetrachloroaurate (99%+) was purchased from Alfa Aesar (Ward Hill, MA, USA). Sodium citrate tribasic dihydrate (99%+), cetyltrimethylammonium bromide (CTAB, 99%+),
tetraethylorthosilicate (TEOS), and 3-aminopropyltrimethoxysilane (APTMS) were purchased from Sigma-Aldrich (St. Louis, MO, USA). Sodium hydroxide (beads) was purchased from Fisher Scientific (Pittsburgh, PA, USA).

**Laser Irradiation.** A COHERENT CUBE 445-40C diode laser (Santa Clara, CA, USA) was used to irradiate Au@MSN NPs at 448 nm. A COHERENT Argon Innova 90C-5 ion laser (Santa Clara, CA, USA) was applied to excite Au@MSN NPs at 514 nm. A COHERENT Ar/Kr+ laser (Santa Clara, CA, USA) was applied on Au@MSN NPs at 530, 568, and 647 nm. The powers of irradiations specified in the article (15, 20, 30, 50, and 100 mW) take into account the different mirrors, lenses, and glass objects in the path the laser beam. The laser spot was half of a centimeter in diameter; thus, the Au@MSN were submitted to 0.06, 0.08, 0.12, 0.2, and 0.4 W/cm². A dried powder of Au@MSN or Au@MSN@Polymer (~2 mg) was deposited at the bottom of a quartz cuvette. A controlled amount of deionized water (2 mL) was then slowly added using a micropipette to avoid dispersing the particles. The selected laser was then directed at the powder and the degradation or release experiments were carried out. In this configuration, not all NPs receive the same number of photons, but it enabled the simultaneous tracking of cargo molecules released from the NPs without disturbing the system (change of concentration or dispersion, etc).

**Au NPs 15 nm.** Monodisperse Au NPs were obtained from the reported Turkevich method involving the reduction of potassium tetrachloroaurate complexes (55 mg, 11 mM) via the injection of sodium tribasic citrate reducing agent (120 mg, 40 mM) in boiling water (100 mL) for 5 min [59]. The resulting solution A was utilized without further preparation.

**Au@MSN with Monodisperse Cores.** An aqueous solution (90 mL) of sodium hydroxide (875 µL, 2M), and CTAB (250 mg) was stirred vigorously at 80 °C. Then, a solution of 15 nm Au NPs (30 mL of A) was added to the aforementioned mixture. Finally, TEOS (1200 µL) was added by consecutive dropwise additions. The sol–gel process was conducted for 2 h. Afterward, the solution was cooled at room temperature while stirring; fractions were gathered in propylene tubes and collected by centrifugation during 15 min at 21 krpm. The sample was then extracted twice with an alcoholic solution of ammonium nitrate (6 g·L⁻¹, NH₄NO₃), and washed three times with ethanol, water, and ethanol. Each extraction involved a sonication step of 30 min at 50 °C in order to remove the CTAB surfactant; the collection was carried out in the same manner. The as-prepared material was dried under air flow for a few hours.

**Au@MSN with Polydisperse Cores.** Such a procedure was adapted from a reported one-pot process of Au@MSN NPs [57]. A mixture of water (100 mL), ethanol (40 mL), and CTAB (0.640 g), and potassium tetrachloroaurate (55 mg) was stirred at 70 °C in a three neck 250 mL round bottom flask. Secondly, sodium hydroxide (200 µL, 2M) was injected to produce the nucleation of the NPs nucleation instantaneously. The NPs growth was conducted for 30 min under 600 rpm. Afterward, TEOS (1000 µL) was added by dropwise additions to the stirred aforementioned solution. Then, the condensation process was triggered by a second addition of sodium hydroxide (400 µL, 2M). After 1 min 30 s, the typical purple color of thin coated Au@MSN particles was observed, and the sol–gel process was conducted for 2 h. The material was collected through centrifugation at 7830 rpm for 15 min. Each fraction was washed with MeOH (40 mL) and centrifuged 10 min, three times. The sample was then extracted twice with an alcoholic solution of NH₄NO₃ (6 g·L⁻¹), and washed three times with ethanol, water, and ethanol. Each extraction involved a sonication step of 30 min at 50 °C in order to remove CTAB surfactant; the collection was carried out in the same manner. The as-prepared material was dried under air flow for a few hours.

**Au@MSN@PCL Polymer.** To prepare the silylated PCL polymer used for the mesoporous silica coating, a mixture of PCL diol (ca. 2000 g·mol⁻¹) was mixed with two equivalents of 3-(triethoxysilyl)propyl isocyanate 95% in toluene (50:1, v:v). The solution was refluxed overnight (the reaction spontaneously occurs at high temperature). The solution was then cooled and kept in a fridge to be used without further purification. For the polymer coating reaction, a controlled volume of silylated PCL in toluene was added to Au@MSN (~3:100, w:w), and the coupling was obtained at room temperature by stirring
overnight without a catalyst. The Au@MSN@PCL particles were finally washed twice with water, dried under air, and used for degradation or release experiments. In the case of cargo-loaded Au@MSN@PCL NPs, cargo molecules (~2–3 mg) were first mixed with Au@MSN (~10 mg) and stirred overnight. The next day, silylated PCL was added to the mixture and the same procedure described above was applied.

4. Conclusions

In summary, we reported for the first time the photocracking of silica particles using plasmonic photothermal effects in an Au@MSN nanosystem. The photocracking and advanced dissolution of silica particles were observed by electron microscopy after 30 min of irradiation under low power continuous wave irradiation (e.g., 30 mW), and the same results were also observed after only one minute of laser excitation (data not shown). The silica shell photodegradation was controlled through tuning the power and wavelength of the laser, or by tuning the size of gold nanocores at a given wavelength. In the future, quantitative photodegradation studies could be performed by changing the irradiation setup using stirred particle dispersions with low-volume cuvettes.

Regarding the photodegradation mechanism, since calcination methods abound to remove molecular templates from mesoporous silica and none of them have ever caused the cracking of silica, it follows that temperature alone does not account for the cracking silica, at least up to 600 °C. We believe that the photocracking of silica perhaps occurs in a process similar to thermal fracturing in glass. When a temperature differential is rapidly created within glass, the silicon dioxide network fractures. Another component that may play a concomitant role in the photodegradation is the potential vibration of plasmonic cores. Nonetheless, the silica photocracking mechanism remains largely unknown.

The unique plasmonic photocracking of silica was then successfully harnessed to controllably release cargo molecules encapsulated within Au@MSN@Polycaprolactone nanovectors. The tripartite nanovectors were cracked much like “nano-eggs” to release cargos upon laser actuation. Future works could apply the photothermal cracking of silica for the delivery of drugs with enhanced cytotoxicity under hyperthermia such as DocetaxelTM [62]. Multiple drug delivery could be obtained using non-symmetrical nanoplatforms having gold nanocores of various sizes thanks to the wavelength dependence. Besides, using NIR-sensitive nanocores, such as gold nanorods or nanoshells, would enable drug delivery upon photocracking in the NIR I or NIR II region for clinical applications. One could also envision the use of plasmonic photocracking for the delivery of drugs with enhanced cytotoxicity under hyperthermia such as DocetaxelTM [62]. Multiple drug delivery could be obtained using non-symmetrical nanoplatforms having gold nanocores of various sizes thanks to the wavelength dependence. Besides, using NIR-sensitive nanocores, such as gold nanorods or nanoshells, would enable drug delivery upon photocracking in the NIR I or NIR II region for clinical applications. One could also envision the use of plasmonic photocracking for the delivery of drugs with enhanced cytotoxicity.
point: 60 °C), Figure S13: Thermo-induced controlled release profile of non-porous and porous silica nanoparticles coated with the polymer and loaded with rhodamine B dyes (ΔAbsmax at λ = 553 nm). This control experiment shows that the loading of cargos inside polymer-coated MSN mainly occurs inside the silica pores and not inside the polycaprolactone polymer shells.

**Author Contributions:** The concept, experiments, and manuscript preparation were realized by J.G.C. The release experiment was conducted by T.M.G.-A.

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