Technical Note

Medial Closed Wedge Distal Femoral Osteotomy Using a Novel Plate With an Optimal Compression System

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Abstract: Medial closed wedge distal femoral osteotomy (MCWDO) has been widely performed for lateral-compartment osteoarthritis since the development of a biplanar osteotomy technique using existing MCWDO-specific plates. To further improve this system and the technique, we have developed a newly designed MCWDO plate (TriS-MDFO; Olympus Terumo Biomaterials). The improved shape of the plate consists of a larger head–shaft angle to fit the distal femur after MCWDO, more distally oriented distal screws to enable longer screw insertion, and a diamond-shaped plate head to avoid interference with the medial patellofemoral ligament. Technically, to overcome the difficulty in inserting proximal screws through the vastus medialis muscle, a cannulated screw system was employed. This system can prevent difficulties in removing the screw due to cross-threading when plate removal is required. Furthermore, we designed a novel compression hook device with a bulb-shaped head to hook on a screw hole to apply a compressive force to the osteotomized site. On the plate side, a characteristic 1.5 mm-thickness stopper is installed to prevent slippage of the hook device. This optimal compression system can minimize the risk of lateral hinge fracture during the compression procedure. These improvements in the TriS-MDFO may increase the ease and safety of MCWDO.

Medial closed wedge distal femoral osteotomy (MCWDO) is widely performed for valgus knee with lateral-compartment osteoarthritis when the deformity center is located at the distal femur. Although favorable short- to mid-term results have been reported since the development of a biplanar osteotomy with existing plates,1,2 the following problems remain, especially in the Asian population, who have smaller femurs: (1) the straight shape of the plate, which sometimes requires bending; (2) an inappropriate distal screw direction, which sometimes interposes into the osteotomized site; (3) interference with the medial patellofemoral ligament (MPFL); (4) difficulty in inserting proximal screws, and (5) risk of lateral hinge fracture (LHF) during the application of compression to the osteotomized site using a lag screw. To improve these potential disadvantages, the authors have developed a newly designed MCWDO-specific locking plate made of titanium alloy (TriS Medial DFO Plate [TriS-MDFO], Olympus Terumo Biomaterials, Tokyo, Japan).

Improvement in the TriS-MDFO

Regarding the plate design, a more anatomically shape was adopted to fit the medial cortex after MCWDO without bending. The head–shaft angle of the representative existing plate and the TriS-MDFO is 20° and 40°, respectively (Fig 1 A and B). In addition to the difference in the head–shaft angle, the distal screws are aimed 12° more distally compared with the existing plate (Fig 1 A and B). This improvement enables the insertion of longer screws to achieve greater stability, without interference with the oblique osteotomy line (Fig 1B). Furthermore, a square-shaped head sometimes

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interferes with the MPFL in small femurs, which can result in flexion loss.\textsuperscript{3} We therefore designed a diamond-shaped head to avoid this (Fig 1C and D, and 2).

Regarding the screws, a cannulated screw system was employed. Insertion of proximal screws can be difficult, especially in patients with obesity and in patients with a thick vastus medialis muscle. The cannulated system helps insertion of the screw in an appropriate direction for such patients, even under the mini-incision technique.

In addition to the plate and the screws, we also designed an original compression hook device (Fig 3), which has a proximal bulb-shaped head to hook onto the screw hole. On the plate side, a characteristic 1.5 mm-thickness stopper (Fig 3) is installed to prevent slippage. After the bulb-shaped head is hooked on the stopper, the lateral cortex is held by the hook, allowing compressive force to be applied with a dedicated screwdriver for the hook. In the event of slippage, a Kirschner wire (K-wire) can be inserted into the hook’s cannulated end (Fig 3). The pearls and pitfalls of the TriS-MDFO are described in the Discussion section and listed in Table 1.

**Surgical Procedure (With Video Illustration)**

**Approach**

We use a conventional medial parapatellar straight incision (Fig 4A) and a subvastus approach (Video 1). The muscular branches from the descending genicular artery\textsuperscript{4,5} are coagulated or ligated to prevent bleeding (Fig 4B). Not using a tourniquet allows identification of these branches and monitoring of the popliteal artery pulse.

**Osteotomy**

A biplanar MCWDFO\textsuperscript{1-3} is performed under K-wire guidance with sufficient retraction (Fig 4 B-F; Video 1). The method used to determine the osteotomy lines is listed in Table 2. Although the conventional hinge point\textsuperscript{1,2} was usually set just proximal to the upper border of the lateral condyle, a slightly distal hinge is now recommended to prevent an unstable LHF.\textsuperscript{6} We set the hinge point just distal to the upper border of the lateral condyle and in between the lateral cortex and the contour of the lateral condyle (Fig 5). The distal oblique osteotomy (i.e., transverse cut) is started from

\textbf{Fig 1.} Postoperative radiographs of 31-year-old female patient who underwent medial closed wedge distal femoral osteotomy with TomoFix MDF (Synthes GmbH: Solothurn, Switzerland) in her right knee and with TriS-MDFO in her left knee. (A) Anteroposterior view of the right knee. The head-shaft angle (black lines) of the TomoFix MDF is 20° and the distal screws are oriented approximately 5° distal to the direction of the proximal screws. Because of the discrepancy between the direction of the osteotomy line and the distal screws, the screws just distal to the transverse cut draw closer to the osteotomized line (white arrow). (B) Anteroposterior view of the left knee. The head–shaft angle (black lines) of the TriS-MDFO is 40° and the distal screws are oriented approximately 17° distal to the direction of the proximal screws. Owing to the improvement in the screw direction, the longer distal screws can be inserted more parallel to the osteotomized line. (C) Lateral view of the right knee demonstrates the square-shaped head design (dashed black line) of the TomoFix MDF. (D) Lateral view of the left knee demonstrates the new diamond-shaped head design (dashed black line) of the TriS-MDFO.
Fig 2. Interference of the plate head with the medial patellofemoral ligament (MPFL). Trial plates were installed on a cadaveric knee. Dashed lines indicate the proximal and distal margin of the MPFL. (A) The conventional square-shaped head interfered with the MPFL over a large contact area. (B) The newly developed diamond-shaped head decreases the contact area.

Fig 3. TriS-MDFO Plate and the compression hook device. The red numbers and letters indicate the name of the screw holes. Hole 1 and 2 have stoppers (A). The combination of the bulb-shaped hook base (B) and the screw hole bumpers (A) prevents slippage of the hook during compression. Any slippage can be addressed by inserting a Kirschner wire into the cannulated hole (C).

Table 1. Pearls and Pitfalls of the TriS Medial DFO Plate

| Pearls                                                                 |
|------------------------------------------------------------------------|
| 1. A diamond-shaped plate head instead of a square-shaped head          |
| • Impingement between the plate head and medial patellofemoral ligament can be minimized. |
| 2. More distally aimed distal screws                                    |
| • The longer screws can be inserted in the distal part of the osteotomy. |
| 3. Cannulated structure of the screws                                   |
| • The risk of jamming of the screw head due to cross-threading can be decreased by confirming the appropriate drill hole direction. |
| • Use of a Kirschner wire as a guide enables safe and easy screw insertion through the vastus medialis muscle. |
| • Plate removal is possible with a smaller incision.                   |
| 4. A specifically designed compression hook                             |
| • It is easy to provide perpendicular compressive force to the oblique osteotomy line. |
| • Combination of the bulb-shaped hook base and the screw hole stopper prevents slippage of the hook. |
| • The cannulated structure of the hook helps prevent slippage.          |

| Pitfalls                                                               |
|------------------------------------------------------------------------|
| • The compression hook device should be as perpendicular as possible to the oblique osteotomy line to prevent the medial shift of the proximal part. |
| • The compression hook should not be overtightened to avoid lateral hinge fracture |
| • Monocortical fixation for the most proximal screw hole is recommended to avoid stress concentration at the plate end. |
4 cm proximal to the medial femoral epicondyle and the proximal oblique osteotomy is started at the planned distance from the distal oblique osteotomy (Fig 5, 6 A-C). The ascending osteotomy is created with one-fourth of the anteroposterior width and a length of approximately 3 to 4 cm (Fig 5, 6 D and E). Our target postoperative weight-bearing line is aimed to fall between the center of the intercondylar eminence and the top of the medial eminence.

**Fixation with Plate**

After we remove the bony wedge between the osteotomies, both oblique and ascending cut are completed using a reciprocating saw and chisel (Fig 6 F-I; Video 1). The wedge is then gradually closed and the plate is temporarily fixed with 2 K-wires (Fig 7A). Two distal screws are inserted and locked in place of the distal temporary K-wire. Before each screw is inserted, a round-tip pin, such as a blunt K-wire, is inserted into the drill hole to confirm its direction and to guide insertion of a cannulated screw (Fig 7B).

The compression hook is attached to the hole with a thick stopper and tightened with a dedicated screw-driver to compress the osteotomy site (Fig 7C). The proximal K-wire for the temporary fixation is replaced by a bicortical locking screw and an additional locking

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**Table 2. Determination of Osteotomy Lines**

- Biplanar osteotomy.
- The starting level of the distal oblique osteotomy is set to be about 4 cm proximal to the medial femoral epicondyle.
- The hinge point is set to be slightly distal to the upper border of the lateral condyle and 5 mm from the lateral cortex.
- The starting level of the proximal oblique osteotomy is set to be proximally at the planned distance from the starting point of the distal oblique osteotomy.
- The flange thickness is one-fourth of the anteroposterior width of the starting point of the distal oblique osteotomy.
- The flange length is about 3 to 5 cm, depending on the size of the femur.
screw is added to one of the proximal holes. The hook can then be taken away and more locking screws are inserted into the remaining holes.

Monocortical fixation is recommended for the most proximal hole to prevent stress concentration at the plate end. When the vastus medialis muscle is not easily retractable, a K-wire is inserted through a K-wire sleeve in a drill sleeve between the muscle fibers. After the K-wire penetrates the lateral cortex, a mono-cortical drill hole is made using a cannulated drill. By using the K-wire for guidance in inserting the cannulated screw, cross-threading can be prevented (Fig 7D). A general outline of the surgical procedure is described in Table 3.

**Postoperative Rehabilitation**

Range of motion exercise is started on the first post-operative day and is advanced gradually as tolerated. Full weight-bearing begins 4 to 6 weeks after surgery, depending on the situation of the hinge.

**Discussion**

Our modification of the TriS-MDFO aimed to (1) improve the design issue of the plate itself, (2) overcome the MCWDO-specific technical difficulty in inserting proximal screws, and (3) avoid technical pitfall in using a lag screw. The improved plate design enabled better plate fitting, insertion of longer distal screws, and less impingement on the MPFL. However, the latter 2 technical problems cannot be solved solely via design modification of the plate. One of the most general problems with locking compression plates is jamming of the screw head into the plate hole by cross-threading. Particularly in the MCWDO, the thick vastus medialis muscle may lead to the insertion of proximal screws in the wrong direction. In bicortical fixation, the screw direction can eventually be controlled even when the screw reaches the lateral screw hole. In monocortical fixation, however, it is not necessarily easy to insert a screw in the appropriate direction because of the lack of this directional correction by the lateral screw hole. Furthermore, this cannulated system can prevent cross-threading of monocortical locking screws, simplifying plate removal surgery if needed.

Application of compression to the osteotomized site can also be key to successful MCWDO. Although compression is conventionally applied with a temporary lag screw (TLS),8 this can be problematic. First, sufficient compression cannot be provided in cases of severe osteoporosis. Even when the femur is not osteoporotic, the tightening procedure of the TLS can generate an LHF with medial translation when it is inserted perpendicular to the plate (Fig 8 A and B). A more perpendicular insertion to the oblique osteotomy line, which aims for the far more proximal cortex, would be theoretically ideal (Fig 8C). However, the direction may cause difficulty in inserting the TLS due to the overlap screw and interference between the proximal locking screws and the TLS (Fig 8D). In the TriS-MDFO, application of the perpendicular compressive force to the oblique osteotomy line can be easily provided by grasping the lateral cortex without any interference (Video 1, Fig 8 E and F). Slippage of the proximal end of the hook from the screw hole can be prevented by its characteristic shape and the thick stopper on the screw hole, and eliminated by K-wire insertion into the cannulated hole of the hook (Fig 3).

A number of possible risks and limitations in the use of this plate should be considered. First, to ensure rigid fixation, it is made of a titanium alloy, which is stiffer than pure titanium. In cases with delayed union, the poor elasticity of the plate induces stress concentration at the plate end when micromotion persists, raising the
possibility of stress fracture at the site. Second, the larger head–shaft angle may confer a risk of plate-fracture in return for the better fitting. Data from mid- to long-term follow-up are not yet available, and further careful long-term follow-up studies are required.

In conclusion, the TriS-MDFO Plate with a cannulated system and an optimized compression system represent an improvement over the existing MCWDFO-specific plate and may increase the ease and safety of MCWDFO for valgus knees.

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**Fig 6.** Biplane osteotomy (left knee). (A) The first K-wire for the distal oblique osteotomy is inserted 4 cm from the medial epicondyle in the direction of a tangent of the lateral condyle (yellow dashed line). The tip of the K-wire is emplaced between the lateral condyle (yellow dashed line) and the lateral cortex of the femoral shaft (yellow line). (B) A second K-wire is inserted proximally at the planned distance using a width gauge. (C) The tips of the K-wires do not meet, allowing a chisel or a saw blade to be inserted into the hinge point. (D) The osteotomy lines are drawn with an electrosurgical knife. (E) The rough cut of the ascending osteotomy, leaving the lateral cortex intact to prevent lateral hinge fracture, is performed previous to the oblique osteotomies. (F) The distal and the proximal oblique osteotomies are performed between the 2 K-wires. (G) Owing to the rough cut of the ascending osteotomy, the wedge can be easily removed (yellow arrow) when the proximal and distal oblique osteotomy lines meet together. (H) The posterior cortices are trimmed using a reciprocating saw. (I) To prevent an unstable lateral hinge fracture, it is crucial to cut the lateral portion of the ascending osteotomy line (yellow shaded area) completely. (SP, suprapatellar pouch; VM, vastus medialis muscle.)
Fig 7. Plate fixation (left knee). (A) After gradual wedge closure, the plate is temporarily fixed with 2 K-wires. Because of the interference between sleeves caused by the larger head-shaft angle, it is difficult to use K-wire sleeves of conventional length, and short sleeves are therefore used for the distal part of the osteotomy (yellow dashed line). (B) Distal screws are inserted through a round-tip pin to confirm the appropriate direction. (C) The compression hook is attached to the hole with a thick stopper and tightened with a dedicated screwdriver to compress the osteotomy site. (D) The most proximal monocortical screw (hole 4 of Fig 3) is inserted through a K-wire which penetrates the lateral cortex. The round-tip pin which is inserted into hole 2 or hole 1 also can be used as reference for the appropriate parallel direction of the proximal screws. These procedures can prevent cross-threading. (KW, Kirschner wire; RP, round-tip pin; VM, vastus medialis muscle.)

Table 3. Surgical Procedure

1. Approach
   - Where necessary, perform partial or total meniscectomy/meniscal repair for a torn lateral meniscus.
   - Medial parapatellar straight incision.
   - Subvastus approach.
   - Coagulate or ligate the muscular branches from the descending genicular artery in elevating the vastus medialis muscle.
   - Full-extension position and mid-flexion position are recommended for the anterior and posterior exposure, respectively.
   - Pulsation of the popliteal artery can be easily confirmed if a tourniquet is not applied.

2. Osteotomy
   - At the midpoint of the femoral width, insert the first K-wire from the starting level of the oblique osteotomy toward just below the hinge point.
   - Insert the second K-wire proximally at the planned distance from the starting point, aiming at a point just above the hinge point.
   - Draw the osteotomy lines described in Table 2 with an electrosurgical knife.
   - Cut the ascending osteotomy line, leaving the lateral cortex intact in full knee extension.
   - Perform the distal and proximal oblique osteotomy between the 2 K-wires and remove the wedge.
   - Finish the osteotomy by inserting a chisel and/or a reciprocating saw into the hinge point between the wires.

3. Fixation
   - After the gradual closure of the osteotomized site, fix the plate temporarily with K-wires, and check the lateral view.
   - Insert and lock the 2 distal screws and remove the distal K-wire.
   - Mount the compression hook on a hole with the bumper perpendicular to the oblique osteotomy line.
   - Tighten the hook with a dedicated screwdriver after removing the proximal K-wire sleeve.
   - Replace the proximal K-wire with a bi-cortical locking screw and add an additional proximal locking screw.
   - Take the hook away and insert locking screws into the remaining holes.
Fig 8. Compressive direction and compression devices. (A) Compressive force in a direction perpendicular to the plate (red arrow). (B) The force causes medial translation of the proximal fragment with a lateral hinge fracture (red arrow). (C) The ideal compressive direction may be perpendicular to the osteotomized line (blue arrow). (D) When the compressive force is applied with a temporary lag screw, the screw direction may hinder insertion of the screw tip into the lateral drill hole due to the overlong screw. The temporary lag screw causes interference with the proximal locking screws. (E) The compression hook is mounted as perpendicularly as possible to the osteotomized line and tightened to provide compressive force (blue arrow). The direction provides an appropriate compressive force to the osteotomized site without lateral hinge fracture (black arrows). (F) As the compression hook does not penetrate the femoral shaft, interference between the compression hook and locking screws is avoided.

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