Modified Subtraction Coronary CT Angiography with a Two-Breathhold Technique: Image Quality and Diagnostic Accuracy in Patients with Coronary Calcifications

Weifeng Guo, MD1, 2, Pratik Tripathi, MD1, Shan Yang, MD1, Juying Qian, MD, PhD3, Bimal Rai, MD4, Mengsu Zeng, MD, PhD1, 2

Departments of 1Radiology and 3Cardiology, Zhongshan Hospital, Fudan University, Shanghai, China; 2Shanghai Institute of Medical Imaging, Shanghai, China; 4Department of Radiology, Tongji Hospital, Tongji Medical College, Huazhong University of Science and Technology, Wuhan, China

Objective: To evaluate a modified subtraction coronary computed tomography angiography (CCTA) technique with a two-breathhold approach in terms of image quality and stenosis grading of calcified coronary segments and in the detection of significant coronary stenosis in segments with severe calcification.

Materials and Methods: The Institutional Review Board approved this study, and all subjects provided written consent. A total of 128 patients were recruited into this trial, of which 32 underwent subtraction CCTA scans and invasive coronary angiography (ICA). The average Agatston score was 356 ± 145. In severely calcified coronary segments, the presence of significant (> 50%) stenosis was assessed on both conventional CCTA and subtraction CCTA images, and the results were finally compared with ICA findings as the gold standard.

Results: For severely calcified segments, the image quality in conventional CCTA significantly improved from 2.51 ± 0.98 to 3.12 ± 0.94 in subtraction CCTA (p < 0.001). In target segments, specificity (70% vs. 87%; p = 0.005) and positive predictive value (61% vs. 79%; p < 0.01) were improved using subtraction CCTA in comparison with conventional CCTA, with no loss in the negative predictive value. The segment-based diagnostic accuracy for detecting significant stenosis was significantly better in subtraction CCTA than in conventional CCTA (area under the receiver operating characteristic curve, 0.94 vs. 0.85; p = 0.03).

Conclusion: This modified subtraction CCTA method showed lower misregistration and better image quality in patients with limited breathhold capability. In comparison with conventional CCTA, modified subtraction CCTA would allow stenosis regrading and improve the diagnostic accuracy in coronary segments with severe calcification.

Keywords: 320-detector row CT; Coronary CT angiography; Plaque calcification; Subtraction

INTRODUCTION

Multidetector coronary computed tomography angiography (CCTA) is the first-choice examination modality for patients suspected of having coronary artery disease (1-3). However, blooming and beam-hardening artifacts due to the presence of severe coronary calcification or implanted stents are still major problems for accurate evaluation of segment-based coronary stenosis (4, 5). Therefore, some studies have reported that CCTA should not be performed as the next step in the diagnostic workup of patients with a high coronary artery calcification score (6, 7).

Recently, a new postprocessing technique called subtraction CCTA has been introduced. In subtraction CCTA, plaque calcifications in the coronary arteries were eliminated by subtracting precontrast CT image data from
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postcontrast CCTA image data. Promising results have been reported by applying subtraction CCTA in patients with severe coronary calcifications or stents (8-15).

In subtraction CCTA, one-breathhold and two-breathhold scanning techniques have been used. In previous studies, researchers mainly focused on a long-lasting one-breathhold scan protocol in subtraction CCTA (9-13). The one-breathhold approach requires a relatively longer breathhold for the acquisition of precontrast and postcontrast image data. Many elderly patients with high coronary calcium suffer from obstructive lung disease and may not be able to hold their breath for such a long time, and thus, a two-breathhold approach would be suitable in this scenario. Nevertheless, misregistration artifacts have been shown to be pronounced due to misalignment between contrast and mask images during the subtraction process, which has been observed in approximately 50% of all target segments using the original two-breathhold scanning protocol (14, 15).

To further minimize misregistration artifacts, we propose a modified two-breathhold subtraction approach (Fig. 1) in patients who are unable to perform a long breathhold. The aim of our study was to evaluate the applicability of subtraction CCTA using this modified scanning protocol in terms of image quality and stenosis grading of calcified coronary segments and in the detection of significant coronary stenosis in coronary segments with severe calcification in comparison with conventional CCTA.

MATERIALS AND METHODS

Study Population

All patients who met the inclusion criteria agreed to participate in the study and signed an informed consent form. The study protocol was approved by the Institutional Review Board from our hospital.

Patients with suspected or known coronary artery disease were prospectively enrolled from August 2016 to December 2017. For cases involving routine CCTA, exclusion criteria were a history of allergic reaction to iodinated contrast agents, arrhythmia, previous cardiac surgery, evidence of acute coronary syndrome, New York Heart Association functional class III or IV heart failure, aortic stenosis, and intolerance to beta-blockers.

For subtraction CCTA scans, the inclusion criteria were heart rate (HR) ≤ 65 beats per minute (bpm) after oral administration of beta-blocker (Betaloc, 25 mg; AstraZeneca, London, UK) or basal HR ≤ 65 bpm and coronary artery calcification detected in the proximal segments. Proximal coronary segments were defined as previously described (9). Patients were excluded for further mask scans due to motion artifacts in contrast images.

During the study period, a total of 164 patients underwent subtraction CCTA due to coronary artery calcification or stent placement. Of these 164 patients, 36 patients (33 with coronary stents, 2 with motion artifacts, and 1 with insufficient coronary lumen contrast enhancement) were excluded from the study. Finally, 128 patients who had undergone subtraction CCTA scanning were included for further analysis, of which 32 (25%) underwent CCTA with invasive coronary angiography (ICA) as the reference standard to determine the diagnostic value.

ICA

ICA using the standard technique was performed in clinically indicated subjects within 60 days of subtraction CCTA scanning. ICA (Anigostar Plus; Siemens Healthineers, Berlin, Germany) was performed using standardized angiographic techniques. Quantitative coronary analysis (QCA) was performed using a software program (SyngofastView, VX57133; Siemens Healthineers) by a cardiologist with more than 15 years of experience. Significant stenosis was defined as > 50% luminal reduction in the most severe stenosis in the calcified segments.

CCTA Data Acquisition

All scans were performed using a 320-detector row CT scanner (Aquilion ONE VISION Edition; Canon Medical Systems, Otawara, Japan) with 0.5-mm detector elements and a gantry rotation time of 275 ms. Images
were reconstructed with a 512 x 512 matrix and 0.5-mm thickness by using standard kernel FC09 iterative reconstruction (AIDR 3D; Canon Medical Systems). Beta-blockers were given when the resting HR was above 65 bpm unless patients had contraindications. Sublingual short-acting nitroglycerin (0.5 mg; Yimin Pharma, Beijing, China) was routinely given during data acquisition.

Noncontrast CT scanning was performed for all patients to determine the calcification score using the method described by Agatston et al. (16). Noncontrast cardiac CT scans were obtained with a tube voltage of 120 kV and a tube current of 50 mA. Mid-diastolic or end-systolic images were acquired using the prospective gating method. The scan range included the region from the origin of the aorta to the apex of the heart. The reconstruction slice thickness was 3 mm.

We adopted a modified two-breathhold approach in this study (Fig. 1). After the contrast imaging acquisition, the investigator determined whether the target coronary segments needed the mask images for postprocessing subtraction. It took at least 60 seconds after the contrast injection until the next noncontrast scan. Theoretically, there was no contrast residue in the coronary artery system and left cardiac chamber during mask scanning. Both the contrast and mask image data were acquired by using a prospective electrocardiography triggering technique between 65% and 80% of the RR interval. Scanning was performed with a tube voltage of 120 kVp and a rotation time of 275 ms. The tube current setting was selected based on the value calculated by the automatic exposure control function (17) with the standard deviation (SD) value set to 20 HU.

The contrast-enhanced scan was performed using iodinated contrast medium with an iodine concentration of 370 mg/mL (Ultravist® iopromide-370; Bayer AG, Berlin, Germany) injected at a rate of body weight (kg) x 0.06 mL/s in 10 s (fixed), followed by a 30-mL saline chaser bolus. The effective radiation dose was estimated based on the dose-length product (DLP, mGy x cm) by using the formula of effective radiation dose = DLP x κ, where κ = 0.014 mSv x mGy⁻¹ x cm⁻¹ (18).

Subtraction Postprocessing

Subtraction was performed using a dedicated algorithm “volumetric CT digital subtraction angiography” (19) that was available on the scanner console. First, a global nonrigid registration was performed, followed by a local rigid registration for the targeted coronary segment. Thus, the results obtained reflected only the contrast filling the coronary artery without calcification.

Image Analysis

The acquired conventional and subtraction CCTA images were transferred to a workstation (Vitrea, version 6.5.3; Vital, Minneapolis, MN, USA) to generate a curved planar reformation image and a cross-sectional image. The coronary arteries were divided into 17 segments according to the American Heart Association classification. Plaque calcification within each coronary segment was determined as follows: in addition to the most severe plaque calcification identified by CCTA using a cross-sectional grading method as previously described (20), we assessed the plaque calcification associated with the maximum cross-sectional arc within each segment as defined by CCTA for this investigation. To analyze the stenosis in the targeted segment, the minimum lumen diameter was measured at the site with the highest degree of arc calcifications within each segment. On the basis of the extent of segment calcification determined using an adapted cross-sectional arc calcification method (21), the targeted calcified plaques were classified as mild calcification (cross-sectional arc calcium < 90°), moderate calcification (cross-sectional calcium arc 90°–180°), and severe calcification (cross-sectional calcium arc > 180°) (Fig. 2).

Segmental image quality was evaluated for each calcified segment using a 4-point scale: 1 = uninterpretable, 2 = poor image quality, 3 = adequate image quality, 4 = good image quality. Segments with two points due to distinct misregistration were deemed nondiagnostic and were considered to be equivalent to severe stenosis for subsequent analysis.

Quantitative assessment of the stenosis was performed in cross-sectional and longitudinal projections by two experienced cardiac radiologists with more than 10 years of experience. The radiologists were blinded to the results of ICA but were aware of the clinical history of the patients. Stenosis was graded as minimal, mild, moderate, and severe, corresponding respectively to stenosis of ≤ 25%, 26–50%, 51–75%, and ≥ 76%, as recommended by the Society of Cardiovascular Computed Tomography (22). Discrepancies were settled by consensus. Note that if the targeted segment was judged to be non-assessable, the image findings were classified as severe stenosis.
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Statistical Analysis

We evaluated the data on a segment level. The average image quality scores between conventional and subtraction CCTA images were compared using a paired t test. The diagnostic vs. nondiagnostic image quality frequencies were compared using the McNemar test. The kappa coefficient was used to measure agreement between conventional and subtraction CCTA for targeted segment stenosis grading. For all the ICA examinations performed, the conventional and subtraction CCTA diagnostic accuracies (sensitivity, specificity, positive predictive value, and negative predictive value) for detecting significant stenosis (>50%) were assessed in segments with severe calcification, and p values for comparison between diagnostic tests were calculated by the McNemar test. To assess diagnostic accuracy, the area under the curve (AUC) of the receiver operating characteristic (ROC) was calculated for both conventional CCTA and subtraction CCTA. The method proposed by DeLong et al. (23) was used for comparison of the two ROC curves. Statistical analyses were performed using the Statistical software MedCalc version 11.5.0.0 (MedCalc Software, Ostend, Belgium). Metric variables were expressed as the mean ± SD. All tests were two-tailed with a significance threshold of p values less than 0.05 and a confidence interval (CI) of 95%.

RESULTS

The clinical, demographic, and radiological characteristics of the 128 included patients are shown in Table 1. Of these patients, 25% (32/128) with 58 severely calcified segments further received ICA as the reference standard for detection of significant stenosis to evaluate the diagnostic value of this modified subtraction technique. The average Agatston score was 356 ± 145. The total effective radiation dose for the subtraction CCTA scan was 5.3 ± 1.2 mSv. The mean HR was 57 ± 6 bpm (range, 46–63 bpm) during the contrast scan and 57 ± 8 bpm (range, 47–65 bpm) during the mask scan.

Table 1. Patient Characteristics (n = 128)

| Characteristics                     | Values     |
|-------------------------------------|------------|
| Age (years)                         | Mean ± SD  67 ± 8 |
|                                     | Range      | 48–84     |
| Sex (n)                             | Male       | 80 (62.5%)|
|                                     | Female     | 48 (37.5%)|
| Body mass index (kg/m²)             | Mean ± SD  23.6 ± 3.8 |
|                                     | Range      | 17.2–30.0 |
| Coronary risk factors (n)           | Hypertension | 70 (54.7%) |
|                                     | Diabetes   | 42 (32.8%)|
|                                     | Hypercholesterolemia | 62 (48.4%) |
|                                     | Smoking    | 48 (37.5%)|
| Coronary calcium score              | Mean ± SD  356 ± 145 |
|                                     | Range      | 36–849    |
|                                     | Median     | 348       |
|                                     | Interquartile range | 132–568   |
| HR at contrast scan (bpm)           | Mean ± SD  57 ± 6 |
|                                     | Range      | 46–63     |
| HR at mask scan (bpm)               | Mean ± SD  57 ± 8 |
|                                     | Range      | 47–65     |
| Estimated effective radiation dose (mSv) | Mean ± SD  5.5 ± 1.7 |
|                                     | Range      | 3.5–9.2   |

bpm = beats per minute, HR = heart rate, SD = standard deviation
Image Quality Analysis between Conventional CCTA and Subtraction CCTA

A total of 128 patients with 564 calcified coronary segments underwent subtraction scanning. With regard to the global calcified segments, the mean coronary image quality score with conventional CCTA was 3.30 ± 0.86 and 3.56 ± 0.62 with subtraction CCTA (p < 0.01). On the basis of conventional CCTA images, 106 (82.8%) patients with 216 (38.3%) segments were judged to have mild calcification, and 94 (73.4%) patients with 185 (32.8%) segments were judged to have moderate calcification. However, image quality in subtraction CCTA did not change significantly in segments with mild calcification (3.68 ± 0.54 to 3.71 ± 0.49, p = 0.68) and segments with moderate calcification (3.49 ± 0.65 to 3.56 ± 0.59, p = 0.48) (Fig. 3). Eighty-four of the 128 subjects were judged to have severe calcification, with severe calcification observed in 163 (28.9%) of the total segments. In the segments showing severe calcifications, after the subtraction of beam-hardening artifacts, the image quality significantly improved from 2.51 ± 0.98 to 3.12 ± 0.94 (p < 0.001) (Fig. 3). Misregistration artifacts were recorded in 17 segments (8%) in the group with mild calcification, 24 segments (13%) in the group with moderate calcification, and 42 segments (26%) in the group with severe calcification.

Stenosis Regrading with Subtraction CCTA in Comparison with Conventional CCTA

For the stenosis grading in conventional CCTA and subtraction CCTA, the kappa index was 0.88 (95% CI, 0.80–0.95; p < 0.001) in the group with mild calcification and 0.84 (95% CI, 0.75–0.92; p < 0.001) in the group with moderate calcification. We observed good agreement values between the mild and moderate calcification groups. Nevertheless, for segments with severe calcification, there was a fair correlation between conventional CCTA and subtraction CCTA for the assessment of stenotic grading, with a kappa index of 0.57 (95% CI, 0.44–0.70; p < 0.001). Of the 163 segments with severe calcification, 52 (32.0%) were changed to a different stenotic class after subtraction, among which 21 (40.4%) were downgraded from moderate to mild stenosis, 17 (32.7%) were downgraded from severe to moderate stenosis, 8 (15.4%) were downgraded from severe to mild stenosis, and 6 (11.5%) were upgraded from mild to moderate stenosis. Segments showing grade changes in the mild and moderate calcification groups were less frequent at 11.1% (24/216) and 16.2% (30/185), respectively. Figure 4 shows the cases of stenosis regrading after subtraction.

Subanalyses of Diagnostic Accuracy in Target Segments with Severe Calcifications

A total of 25% (32/128) of patients with 58 severely calcified lesions underwent subtraction CCTA scans followed by ICA. In the group with severe calcification, nondiagnostic segments with conventional CCTA were obtained in 33% (19/58) of the cases, and after subtraction, the corresponding percentage was 10% (6/58) (p < 0.01). Statistical performance of conventional CCTA and subtraction CCTA to detect coronary artery stenosis > 50% is shown in Table 2. The AUC for the diagnosis of significant stenosis as determined by QCA (Fig. 5) was 0.94 (95% CI, 0.86–1.00) in subtraction CCTA, which was higher (95% CI, 0.74–0.96) than that for conventional CCTA (0.85; p = 0.03). An example is shown in Figure 6.

DISCUSSION

The current study provided a preliminary assessment of the practicability of modified subtraction CCTA with a two-breathhold method in patients unable to maintain a sufficiently long-lasting single breathhold. With this modified approach, image quality was significantly better in
coronary segments with severe calcification of subtraction CCTA compared to conventional CCTA. Although increased misregistration artifacts were observed in segments with severe calcification, a relatively low frequency of misregistration was observed in this modified subtraction CCTA. For segments with severe calcification, the modified subtraction CCTA would change the stenosis grade and improve the diagnostic accuracy in comparison with conventional CCTA using ICA as the gold standard.

One of the challenges for conventional CCTA in stenotic evaluation is the presence of severe calcification or stents, which interfere with the visualization of the coronary

Fig. 4. Case showing stenosis regrading in conventional CCTA and subtraction.
A, B. Moderate calcification is observed in left ascending artery on conventional images. C. After performing subtraction, calcification is eliminated. D-F. Degree of stenosis is assessed as mild in both subtraction and conventional CCTA. Corresponding subtraction process for severe plaque calcification at left anterior descending coronary artery from another patient. Moderate stenosis can be seen in subtraction CCTA, while severe stenosis is rated in conventional CCTA.
lumen and reduce the diagnostic accuracy. The specificity for diagnostic performance has been shown to decrease significantly in patients with severe coronary artery calcification in a multicenter study using a 64-detector CT (24). Subtraction CCTA using dedicated postprocessing software has been shown to improve diagnostic accuracy over conventional CCTA in patients with severe calcification (9, 10). Additionally, it has also been demonstrated that subtraction CCTA is useful in patients with coronary stents (11, 12, 14, 15).

In subtraction CCTA, one- and two-breathhold acquisition protocols have been used to obtain the mask image data. A one-breathhold approach requires a long breath-holding time, and even a modified one-breathhold scan protocol tested by Yoshioka et al. (13) required approximately 15 seconds of breath-holding time to provide diagnostic images. Many elderly patients with a high coronary artery calcium score and obstructive lung disease may not be able to hold their breath for such a long time. Moreover, misregistration artifacts have been shown to be more pronounced (approximately 50% of all target segments) in previous two-breathhold approach studies due to different HR or breathhold variability between the noncontrast and the contrast data sets (14, 15). To further reduce the frequency of misregistration artifacts in subtraction CCTA, we propose a modified subtraction CCTA method with a two-breathhold technique.

In comparison with conventional CCTA, the modified subtraction CCTA protocol resulted in subtraction images with improved image quality. Misregistration artifacts were observed in 26% of target segments with severe calcification, which was significantly lower than the previous study (approximately 50%) designed with the original two-breathhold method.

In our study, stenosis regrading mostly occurred in coronary segments with severe calcification, which implies that the subtraction technique would have more effective clinical significance for this type of calcification. In addition, the diagnostic accuracy of modified subtraction CCTA was improved by its increased specificity and positive predictive value for the assessment of coronary artery stenosis when compared to conventional CCTA. The AUC of the modified subtraction CCTA (0.94) was significantly higher than that of conventional CCTA (0.85) ($p = 0.03$).

These results indicate that modified subtraction CCTA using a modified two-breathhold technique may have adequate accuracy in the diagnosis of significant stenosis in segments with severe calcification.

Some limitations of this study should be acknowledged. First, the small sample size with a small number of calcification segments limited the generalizability of our conclusions. Second, only patients with optimum HR < 65 bpm were eligible for modified subtraction CCTA scanning. Third, misregistration artifacts specific to subtraction CCTA

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**Table 2. Diagnostic Accuracy of Conventional CCTA and Subtraction CCTA in Segments with Severe Calcification**

| Measure               | Conventional CCTA | Subtraction CCTA | $p$  |
|-----------------------|-------------------|------------------|------|
| Sensitivity           | 95%               | 91%              | 0.40 |
| Specificity           | 70%               | 87%              | < 0.01 |
| Positive predictive value | 61%          | 79%              | < 0.01 |
| Negative predictive value | 96%          | 94%              | 0.70 |
| Accuracy              | 79%               | 89%              | 0.05 |
| AUC (95% CI)          | 0.85 (0.74–0.96)  | 0.94 (0.86–1.00) | 0.03 |

Segment-based analysis, $n = 58$. AUC = area under curve, CCTA = coronary computed tomography angiography, CI = confidence interval

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**Fig. 5. Area under receiver operating characteristic curves of conventional CCTA and subtraction CCTA versus invasive coronary angiography: AUC for conventional CCTA is 0.85 (95% CI, 0.74–0.96). AUC for subtraction CCTA is 0.94 (95% CI, 0.86–1.00).** AUC = area under curve, CI = confidence interval
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are still generated in some calcified segments. The final limitation of modified subtraction CCTA is the relatively high radiation dose. In this study, only patients for whom prospective one-heartbeat scanning was possible were selected (25). The average total effective radiation dose in the present study was 5.5 ± 1.7 mSv, which cannot be considered a low value.

To address the problems mentioned above, material density images using dual-energy CT have been reported to reduce or remove the depiction of coronary calcification (26). Theoretically, misregistration can be considered to be negligible due to the use of fast tube voltage switching. Therefore, if iodine and hydroxyapatite can be completely separated, this technique is an ideal method for the evaluation of severely calcified coronary artery segments. Additionally, some studies adopted novel advanced postprocessing algorithms, such as “sharpen” reconstruction (27) and the deblooming algorithm (28), to decrease the blooming artifacts from heavy calcification and consequently improve the diagnostic accuracy of CCTA in assessing coronary stenosis. Moreover, recent advances in computational fluid dynamics and individual image-based modeling permit noninvasive calculation of fractional flow reserve derived from CCTA (FFR-CT). As demonstrated

Fig. 6. 68-year-old man with suspected coronary artery disease.
From CPR image (A) and cross-sectional image (B) in conventional CCTA, severe calcification is observed in proximal portion of left anterior descending artery, which makes it difficult to assess lumen (arrow). In cross-sectional image (C) and CPR cross-sectional image (D) after subtraction, no significant stenosis is depicted (arrow). There is no significant stenosis determined by invasive coronary angiography (arrow) (E). CPR = curved planar reformation
by Nørgaard et al. (29), FFR-CT provided higher diagnostic performance and discrimination of ischemia in patients with high calcification scores in comparison with CCTA assessment. In the future, noninvasive functional assessment based on CCTA will become an important tool for the diagnosis of coronary artery disease. In summary, the results of this preliminary study have shown that the modified subtraction CCTA with a two-breathhold approach allows for stenosis regrading and improves the diagnostic accuracy in patients with segment-based severe calcification and limited breath-holding capability.

**Conflicts of Interest**
The authors have no potential conflicts of interest to disclose.

**ORCID iDs**
Mengsu Zeng  
https://orcid.org/0000-0001-6054-0824  
Weifeng Guo  
https://orcid.org/0000-0003-2377-3279

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