Young's Modulus and Degree of Conversion of Different Combination of Light-Cure Dental Resins

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Abstract: Objectives: To evaluate Young's modulus and degree of conversion of several combinations of bisGMA, UEDMA, TEGDMA light-cure dental resin.

Methods: Young's modulus and DC% were studied for 21 different resin combinations of bisGMA, TEGDMA and UEDMA. Small universal testing machine and photo-calorimetry were used for the tests. The results were evaluated using ANOVA and Duncan's multiple range tests and regular t-test.

Results: Young's modulus varied between 2.37±0.2 GPa (100% TEGDMA) and 4.15±0.2 GPa (100% bisGMA). By adding TEGDMA to bisGMA or UEDMA, the Young's modulus decreased significantly (p<0.05). Degree of conversion was significantly (p<0.05) higher when the wt% of TEGDMA was high in the mixtures than for highly concentrated bis-GMA (resin mixtures with TEGDMA in comparison to mixture with bisGMA had higher degree of conversion). DC% was significantly higher (p<0.05) for binary mixtures of UEDMA and TEGDMA, and significantly lower for 100 wt% bis-GMA (p<0.05). The DC% values were between 53.1%±0.9% (100% bisGMA) and 85.6%±1% (80% UEDMA-20% TEGDMA). The concentration of bisGMA, in the monomer mixture, affected DC% and Young's modulus oppositely.

Conclusions: The differences in the values for DC% were mostly justified by the differences in the molecular structures of the different monomers. It was also revealed that higher DC% does not always result in a higher Young's modulus, because molecular and network structural parameters play major roles in the final physical properties of the mixtures.

INTRODUCTION

A potential problem with dental composite resins is incomplete polymerization which can result in poor mechanical properties. It is therefore important to identify the optimum resin combination(s) that result in high polymerization level and good mechanical properties.

Degree of conversion (DC) is used to determine polymerization level of dental composite resins [1-3], and is related to mechanical properties [4], biocompatibility [5], colour stability [6]. DC is also believed to be related to the clinical performance of the restoration. It is therefore important to identify the best monomer combinations capable of producing high degree of conversion and good mechanical properties of visible light cure dental (VLCD) composite resins.

Many methods can be used to measure the degree of conversion, and the percentage of consumed aliphatic carbon double bonds during polymerization are often used to express the DC value. Some of the most common methods that have been used are nuclear magnetic resonance spectroscopy [7,8], differential scanning calorimetry [9-18], Raman spectroscopy [19,20], conventional infrared spectroscopy [21-25] and Fourier transform infrared spectroscopy (FTIR) [26-31].

Light cure dental composites typically show limited conversion values, and the conversion values range between 40 to 80 percent [9,20,23-25,29]. The low conversion values can be related to the cross-linked polymer network structure that imposes severe restrictions on the mobility of reacting species. To improve conversion, diluents with viscosities up to five orders of magnitude lower than that of a resin like bisGMA are usually used. These diluents are added to facilitate filler addition and mixing. Both the improved conversion level and the increased filler fraction contribute to improving the mechanical properties of the composite. The increased molecular mobility caused by the incorporation of diluents can increase the conversion level 2.5 times over that of pure bisGMA (from 26% for pure bisGMA to 66% for 50/50 bisGMA/TEGDMA) [32]. Structural differences within the diluents contribute to variations in conversion because of differences in segmental motion of the methacrylate based matrices [33]. However, differences in properties of different methacrylate based matrices complicate the interpretation of correlations between conversion and mechanical properties of VLCD composites. For example, by increasing the concentration of TEGDMA mixed with bisGMA, the measured flexural strength decreases despite of an increase in conversion [34,35].

Dental light cure resin composites consist of differently processed filler particles mixed with different monomer systems. Monomer system consisting of bisphenol A glycerolate (1 glycerol/phenol) dimethacrylate/tri[ethylene glycol] di-
methacrylate (bisGMA/TEGDMA), 50:50 by weight, has been used in some products. The high viscosity of bisGMA slows down filler sedimentation in the composite and gives the material a firmer touch. A drawback with the high viscosity, though, is that it makes filler incorporation more cumbersome. In addition, the structure of the bisGMA molecule makes the molecule stiff, which decreases the conversion level of the monomer as the bisGMA content increases. To decrease monomer viscosity, facilitate filler incorporation and enhance degree of conversion, a diluting monomer such as TEGDMA is added. A shortcoming with adding TEGDMA is that the shorter molecule and its higher conversion level increase the polymerisation shrinkage of the matrix. Because of the lower viscosity, though, the increased shrinkage can to some extent be compensated by increased filler incorporation. However, to decrease shrinkage, and still retain good conversion, some manufacturers add UEDMA to the bisGMA/TEGDMA mixture. UEDMA is a more flexible molecule than the bisGMA molecule and cures more efficiently than bisGMA. It also has lower viscosity than bisGMA, making filler incorporation easier. However, despite these advantages, UEDMA has not been able to replace bisGMA completely. The reason is that UEDMA based resins do not have the same handling characteristics as a matching bisGMA system.

Because of the importance of identifying a monomer mixture with low viscosity and low shrinkage but also high conversion, we need to identify the bisGMA:UEDMA:TEGDMA combination that produces the superior matrix material in terms of high conversion levels and high stiffness within acceptable viscosity ranges. Therefore, the objective with this study was to evaluate Young’s modulus and degree of conversion of several combinations of light-cure dental resins e.g., bisGMA, UEDMA, TEGDMA.

MATERIALS AND METHODS

Material groups: In Table 1 materials used in this study are shown. To make the resin matrices light curable, photo initiator (camphorquinone 0.35 wt%) and coinitiator (dimethyllaminoethylmethacrylate (DMAEMA) 0.7 wt%) were added to the monomer mixtures. Twenty-one different resin combinations from the tertiary bisGMA:TEGDMA:UEDMA system were prepared (the weight % of monomers in different mixtures are shown in Tables 2 and 3).

Tensile test specimens: For the tensile test, 6 specimens per resin formulation were prepared.

To ease the handling of the prepared mixtures, all 21 formulations were preheated at 37 °C for

30 min before they were carefully poured into Teflon mould to produce samples 50 mm long, 8 mm wide and 1 mm thick. Once the mould had been filled and covered with Mylar sheets, a weight was placed on the covered mould to compress the liquid and secure proper shape and thickness. The weight was then removed after 15 s and specimen was cured with Osram Dulux laboratory curing (manufactured in Italy) unit with 30 mW/cm² for 10 min. After the specimens had been removed form the mould their sides were polished flat under water with a SiC sand paper (P 600). Specimens made in this way were then stored in darkness for 24 before they were tested.

Tensile testing procedure: Strain gauges (Student gauge type CEA-06-240UZ-120; Measurements Group, Inc., Raleigh, NC, USA) were attached to the specimens at least 24 hours before the test was conducted. Minimat (Model MM11-04, Thermal Sciences, Loughborough, England) was used for Young’s modulus measurement and the specimens were tested in tension at a strain rate of 1% per min. The elastic modulus of each specimen was calculated by measuring the slope of the stress-strain curve between 0.05 and 0.25% of strain.

Degree of conversion: The percentage of aliphatic carbon double bonds reacting during polymerization of the matrix resins were used to measure the degree of conversion. Photocalorimetry (photo-DSC) was used for these measurements. Photo-DSC is based on isothermal differential scanning calorimetry (DSC), which measures the amount of heat released during polymerization. Some of the recorded heat generated during photo-DSC measurement is heat released by the light curing source. The heat generated by the light source is subtracted from the total heat being released during curing, and the resulting heat represents the amount of heat released during curing. By using the energy value released by one mole aliphatic bonds during curing, one can calculate how many percentages of the aliphatic bonds have participated in the polymerization reaction [36].

In isothermal methods, the rate of heat evolution and the reaction rate are recorded as a function of irradiation time. The rate of polymerization (Rₚ), i.e. the rate of monomer conversion is given by:

\[
R_p = -\frac{d[M]}{dt} = \frac{dH}{dt} = \frac{1}{\Delta H_p}
\]
\( \frac{dH}{dt} \) is the ordinate of the curve (J/s), \( \Delta H_p \) is the molar heat of polymerization (J/mol) (based on the full conversion monomer), \( V \) is the total reaction volume (L), and \( [M] \) is the monomer concentration (mol/L). This equation ignores the heat produced by the decomposition of the photo-initiator and the termination reactions.

Assuming that the heat evolved in DSC measurement is proportional to the number of monomer moles reacted, the degree of monomer conversion (\( \alpha \)) as a function of time (t) can be calculated from:

\[
\alpha = \frac{\Delta H}{\Delta H_p} \times 100
\]

(2)

Statistical analysis: The results were tested using ANOVA and Duncan’s multiple range tests and regular t-test. All tests were performed at the p<0.05 level.

RESULTS

Youngs modulus: The moduli of elasticity values, measured 24 hours after the samples had been cured, are shown in Fig. (1). The standard deviation and Waller groupings are also shown in Table 2. Statistical evaluation of the data revealed that the modulus of elasticity was significantly higher for pure bisGMA than pure TEGDMA and pure UEDMA. The statistical evaluation also revealed that different combination of three resins did not affect the modulus of the mixture significantly. As seen from Table 2, Young’s modulus values vary between 2.37 (for 100% TEGDMA) and 4.15 GPa (for 100% bisGMA).

Degree of conversion: Fig. (2) shows degree of conversion values calculated for the cured 21 mixtures. The Waller groupings are also shown in that table. There were significant differences between degree of conversions of the pure resins (p<0.05). Increased amounts of bisGMA always affected the degree of conversion adversely. Pure TEGDMA showed significantly higher degree of polymerization, as well faster polymerization rate. Values going from 53.1% (for 100% bisGMA) to 85.6% (for 80% UEDMA and 20% TEGDMA) of conversion are found. The higher the mixture contents of bisGMA, the lower the degree of conversion while higher concentrations of TEGDMA gave higher degree of conversion values. The presence of UEDMA played an intermediate role between the two monomers, giving usu-

Table 2. Young’s Modulus with Standard Deviation and Waller Grouping for All Mixtures (Shown Number is Mean Values of Six Measurements)

| Mixture (No.) | bisGMA (% wt) | UEDMA (% wt) | TEGDMA (% wt) | E-modulus (GPa) | Waller Grouping |
|---------------|---------------|--------------|---------------|-----------------|----------------|
| 1             | 100           | 0            | 0             | 4.1±0.5         | A              |
| 2             | 0             | 100          | 0             | 3.1±0.2         | DEFGH          |
| 3             | 0             | 0            | 100           | 2.4±0.3         | I              |
| 4             | 80            | 20           | 0             | 3.2±0.6         | CDEFG          |
| 5             | 60            | 40           | 0             | 2.9±0.6         | FGHI           |
| 6             | 40            | 60           | 0             | 3.1±0.6         | DEFG           |
| 7             | 20            | 80           | 0             | 3.6±0.9         | ABCD           |
| 8             | 0             | 20           | 80           | 2.5±0.5         | HI             |
| 9             | 0             | 40           | 60           | 2.4±0.4         | I              |
| 10            | 0             | 60           | 40           | 2.4±0.3         | I              |
| 11            | 0             | 80           | 20           | 2.8±0.4         | HIG            |
| 12            | 80            | 0            | 20           | 4.2±0.8         | A              |
| 13            | 60            | 0            | 40           | 3.4±0.7         | BCDEF          |
| 14            | 40            | 0            | 60           | 3.2±0.6         | DEFG           |
| 15            | 20            | 0            | 80           | 3±0.3           | EFGHI          |
| 16            | 20            | 20           | 60           | 3.3±0.6         | CDEFG          |
| 17            | 40            | 20           | 40           | 3.8±0.6         | ABC            |
| 18            | 60            | 20           | 20           | 3.8±0.8         | AB             |
| 19            | 20            | 40           | 40           | 3.5±0.5         | BCDEF          |
| 20            | 40            | 40           | 20           | 3.5±0.6         | ABCE           |
| 21            | 20            | 60           | 20           | 3.2±0.3         | CDEFG          |
ally degrees of conversion higher than the bisGMA and lower than the TEGDEMA.

**DISCUSSION**

The structural features of the three monomer molecules can explain the modulus results. Of the three monomers, the bisGMA molecule has the least flexible molecular structure because of the two aromatic rings present along the backbone structure. In addition, the chains are also held together by hydrogen bonds formed between pendant OH groups. The molecular stiffness and the hydrogen bond formation are important factors to consider [34,37].

Both the UEDMA and the TEGDMA molecules are more flexible than the bisGMA molecule. The TEGDMA molecule is also significant shorter than bisGMA. Both the bisGMA and the UEDMA molecules have hydrogen bonds, but the higher rigidity of the bisGMA molecule, caused by the presence of the two phenol rings, increases the likelihood of stable hydrogen bond formation of the bisGMA monomer when compared to the more flexible UEDMA molecule. The higher flexibility and ability of chain rotations of both TEGDMA and UEDMA molecules and their lower tendencies of forming stable hydrogen bonds should decrease the rigidity of such polymers. As shown in Fig. (1), the Young’s modulus also increased as the concentration of the bisGMA increased in the monomers’ mixtures [20].

![Fig. (1). Graph showing the modulus values of the different material mixtures. The unit for the modulus is Gpa.](image)
The molecular differences discussed above should also facilitate diffusion of light initiator/co-initiator and increase chain rotations in TEGDMA and UEDMA monomer systems. As a consequence of the increased chain rotation ability, the chance that methylmethacrylate groups react with each other during polymerization should increase. By considering the molecular structures, TEGDMA would be the structure having the highest ability to rotate, move and polymerize and thereby also react easiest. As a consequence, increased TEGDMA should favor an increase in DC. These expectations are also supported by the results presented in Fig. (2) and Table 3.

![Graph showing the conversion values for the different material mixtures. The conversion values numbers are shown as mean values with their standard deviations.](image)

**Fig. (2).** Graph showing the conversion values for the different material mixtures. The conversion values numbers are shown as mean values with their standard deviations. The unit for the conversion level is % consumed (polymerized) methacrylate groups.

For higher concentrations of bisGMA, the strong impact of stiffness and hydrogen bond formation ability can explain why the modulus increases (Fig. 1) despite a decrease in conversion (Fig. 2). The low modulus value at higher concentration of TEGDMA may also be due to that block and/or random polymerization units of bisGMA/TEGDMA form. In such polymers, some of the TEGDMA molecules may not be able to cross-link, because the longer bisGMA molecules keep the growing chains too far apart to allow cross-linkage with the shorter TEGDMA molecules. However, as such a copolymer forms, the bisGMA molecules will be separated from TEGDMA molecules, a separation that will decrease the contribution from hydrogen bond formation between bisGMA molecules. Under such a situation, the stiffness of the polymer should go down and reach a minimum.

Among the bisGMA/TEGDMA combinations, the modulus was highest at 100% bisGMA, and lowest at 100% TEGDMA, while the conversion level much lower for the 100% bisGMA than for 100% TEGDMA. In general, the results suggest that the degree of conversion values increased as the TEGDMA and UEDMA content increased while it decreased as the bisGMA content increased.

By comparing the DC values and the modulus values of the UEDMA/TEGDMA mixtures one can see that the mixtures with highest UEDMA values have high modulus and lower DC values. The higher modulus values can be related to the ability of the UEDMA molecules to form hydrogen bonds, while the increased flexibility of the TEGDMA molecules increases the conversion level.

The differences found between modulus and DC values seen for the rest of the bisGMA/UEDMA/TEGDMA resins can be explained in the same way. Thus, it seems as the highest modulus can be achieved when hydrogen bonding and conversion level are maximized. However, because hydrogen bonding and molecular stiffness increase viscosity and decrease conversion, these processes compete with each other. These findings are important to realize, because they clearly show that high modulus values may not be related to high conversion levels.

**CONCLUSIONS**

Even though there is some correlation between Young's modulus and degree of conversion, a high Young's modulus value does not always mean a high conversion level. The reason such a correlation is not always reliable can be related to the molecular structure of the monomer system and how it affects the polymer network. Therefore, to optimize modulus and conversion level, it is important to identify the best monomer combinations. An optimal combination is one that reduces the residual stress level by decreasing polymerization rate. At the same time, the optimal combination will keep stiffness and degree of conversion at acceptable levels in order to give acceptable mechanical/physical properties of the cured composite.

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