ORIGINAL ARTICLE

Therapeutically relevant structural and functional mechanisms triggered by physical and cognitive exercise

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Physical and cognitive exercise may prevent or delay dementia in later life but the neural mechanisms underlying these therapeutic benefits are largely unknown. We examined structural and functional magnetic resonance imaging (MRI) brain changes after 6 months of progressive resistance training (PRT), computerized cognitive training (CCT) or combined intervention. A total of 100 older individuals (68 females, average age = 70.1, s.d. ± 6.7, 55–87 years) with dementia prodrome mild cognitive impairment were recruited in the SMART (Study of Mental Activity and Resistance Training) Trial. Participants were randomly assigned into four intervention groups: PRT+CCT, PRT+SHAM CCT, CCT+SHAM PRT and double SHAM. Multimodal MRI was conducted at baseline and at 6 months of follow-up (immediately after training) to measure structural and spontaneous functional changes in the brain, with a focus on the hippocampus and posterior cingulate regions. Participants’ cognitive changes were also assessed before and after training. We found that PRT but not CCT significantly improved global cognition (F(90) = 4.1, P < 0.05) as well as expanded gray matter in the posterior cingulate (Pcorrected < 0.05), and these changes were related to each other (r = 0.25, P = 0.03). PRT also reversed progression of white matter hyperintensities, a biomarker of cerebrovascular disease, in several brain areas. In contrast, CCT but not PRT attenuated decline in overall memory performance (F(90) = 5.7, P < 0.02), mediated by enhanced functional connectivity between the hippocampus and superior frontal cortex. Our findings indicate that physical and cognitive training depend on discrete neuronal mechanisms for their therapeutic efficacy, information that may help develop targeted lifestyle-based preventative strategies.

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INTRODUCTION

Cognitive training1,2 and physical exercise3,4 can help support cognitive function in late life, stimulating interest in their potential for the delay or even prevention of dementia.5 Yet, how these lifestyle interventions work in humans is still not clear,6 despite a wealth of studies examining environmental enrichment7,8 and voluntary running paradigms in rodents.9,10 Human neuroimaging studies suggest the induction of some common activity-dependent mechanisms11 as well as biological processes that may be unique to each intervention,12–14 but head-to-head imaging studies are yet to be reported.

One major unresolved question is whether training antagonizes the degenerative effects of advancing age, cerebrovascular disease and Alzheimer’s disease (AD), or stimulates disease-independent mechanisms that cumulatively support cognition. Structurally, the natural history of AD begins with volume loss in entorhinal and hippocampal areas and then progresses to include the posterior cingulate, cortical temporal lobe and eventually most of the gray matter.15,16 It is therefore interesting that physical activity has been linked to preserved hippocampal and frontal cortical volume in cross-sectional17,18 and prospective studies,19 and more direct evidence of possible disease modification provided in a randomized controlled trial (RCT) where 1 year of moderate-intensity walking in healthy elders led to hippocampal expansion compared with atrophy in controls.20 However, the therapeutic relevance of this finding is not clear given the same trial reported equivalent memory change in walkers and controls.21 In contrast, computerized cognitive training is generally efficacious for memory in healthy elderly1 but does not lead to hippocampal structural plasticity. Rather, initial hippocampal volume can independently predict mnemonic improvements at the end of cognitive training.22

Resistance or strength training remains largely unstudied in animal models from a neuroscience perspective. In humans, resistance exercise produces complex systemic and metabolic changes23 and is effective for chronic age-related health issues such as sarcopenia,24,25 osteoporosis26 and insulin resistance.27,28

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Research on the cognitive effects of resistance exercise in older adults is preliminary in comparison with aerobic exercise. One RCT found evidence of improved memory function following 6-month training, whereas two RCTs have found evidence of function improvements, but no memory effects, immediately following training. To date, evidence for cerebral effects of resistance exercise in elders is mixed: one RCT initially reported that resistance exercise led to a small but significant reduction in whole-brain volume, but a subsequent subgroup reanalysis found attenuated white matter atrophy.

Another relevant but poorly modeled mechanism in animals is chronic cerebrovascular disease, typically coexpressed alongside AD pathology in those with dementia or dementia-precursor mild cognitive impairment (MCI). Ischemic and inflammatory brain tissue can be visualized on T2-weighted magnetic resonance imaging (MRI) as white matter hyperintensities (WMHs) and their severity is strongly linked to vascular risk factors. Moreover, WMHs increase risk of cognitive impairment and independently predict transition from MCI to dementia. It is therefore interesting that physical exercise embedded within a comprehensive vascular care program can slow progression of WMHs in older individuals with established dementia. Whether physical or cognitive exercise can produce similar effects on WMH burden in nondemented individuals has not been tested.

Frontal lobe functional connectivity is a candidate for a shared mechanism because it is responsive to both cognitive training and aerobic physical exercise. Frontal lobe connectivity declines with age and has been further implicated in early AD, but whether physical or cognitive exercise is more effective for network rescue is unknown. Another important connectivity pattern is the default mode network (DMN), a spatially distributed but temporally synchronized assembly of brain regions preferentially engaged when a person is internally focused and not attending to external stimuli. A common approach to defining the DMN relies on spontaneous activity in the posterior cingulate (PC). Indeed, this brain region lies at the structural and functional core of the DMN. Whether physical or cognitive training produces functionally relevant changes to the DMN in older adults is not known.

There are hence several possible mechanisms by which cognitive training or physical exercise may achieve therapeutic efficacy but these have not been directly compared in a rigorous RCT setting. At least some of these mechanisms may be specific to physical exercise, and hence supported a prediction of additive therapeutic effects following combined intervention. The Study of Mental Activity and Resistance Training (SMART) Trial was therefore designed to determine whether resistance exercise, cognitive exercise or combined cognitive and resistance training can prevent or slow cognitive and functional decline in individuals with MCI. Here, our aim was to identify therapeutically relevant brain mechanisms using multimodal MRI imaging in the context of a fully factorial, active-controlled, double-blind RCT.

MATERIALS AND METHODS

Subjects and design

SMART trial volunteers (N = 100; 68 females, average age = 70.1 s.d. ± 6.7 years) were nondemented, nondepressed individuals aged ≥ 55 years who met Petersen's original MCI criteria, having subjective memory complaints and a Mini-Mental State Examination score of 24–28 (29 was acceptable only if error noted in memory registration), a Clinical Dementia Rating scale 0 or 0.5 and independence in daily function. Participants were blind to training group hypotheses and assessors were blinded to group allocation. There were no significant differences in dropout (8%), total training time (22.7 weeks), trained sessions per week (2.3 sessions) or absolute compliance (44.6 sessions) between the four interventions groups. Subjective appraisals were measured using the Memory Awareness Rating Scale and Memory Complaint Score. All nonvoxel/vertex-based analyses (that is, cognitive and region-of-interest based MR outcomes) were conducted using linear mixed models, and all analyses controlled for age, sex and education. Sample size calculations were based on the trial's (clinical) primary outcome as reported previously. All participants gave informed consent and the trial was approved by the human research ethics committee of the University of Sydney.

The SMART Trial was prospectively registered with the Australian and New Zealand Clinical Trials Registry (Protocol No: X08-0064).

Interventions

Details about the structure, content and timing of the interventions can be found elsewhere. In brief, they are described as follows.

Cognitive training. CCT comprised the COGPACK program (http://www.cogpack.com/USA/frames.htm), a multidomain computer-based software package developed for neurorehabilitation. Sham CCT was also computer based: participants watched video clips of general interest documentary topics, followed by a set of simple questions regarding the presented material. CCT and sham cognitive training were matched for duration, setting and sensorimotor stimulation. All cognitive training was conducted in a dedicated study center under supervision. Supplementary Information contains the Manual of Procedures for implementing CCT as well as COGPACK definition files for identical replication on this software.

Physical exercise training. PRT was supervised by experienced research assistants (exercise physiologists and physiotherapists) in a physician-supervised clinic at the University of Sydney Exercise campus in a ratio of 1 trainer to 4–5 subjects. Pneumatic resistance machines (Keiser Sports Health Equipment, Fresno, CA, USA) were used for training at high intensity, 3 sets of 8 repetitions of each of 5–6 exercises/session for most major muscle groups (chest press, leg press, seated row, standing hip abduction, knee extension). Sham physical exercise included stretching and seated calisthenics, designed not to notably increase heart rate or aerobic capacity or improve balance or strength.

MRI scanning protocol

MRI data were acquired on a 3.0-Tesla Philips Achieva System (Amsterdam, The Netherlands). For each time point, brain structure was assessed using a T1-weighted whole-brain scan (sequence: T1FFE, TR/TE: 6.39/2.9 ms; slice thickness 1.0 mm without gap; field of view: 256 × 256; resolution 1 × 1 mm) and a T2-weighted FLAIR (Fluid-Attenuated Inversion Recovery) scan (resolution: 0.488 × 0.488 × 3.5 mm; TR/TE = 10 000/110 ms). A resting-state functional MRI (fMRI) was conducted using T2* echo-planar BOLD sequence (TR/TE = 2000/30 ms, 200 volumes, 6.5 min) with the subject's eyes closed.

MRI preprocessing

T1 structure image preprocessing. Three MRI preprocessing methods were applied to examine the change of gray matter. (1) Expert hippocampal manual tracing was performed using our previous published protocol. (2) Functional MRI of the brain (FMRIB)'s Integrated Registration and Segmentation Tool (FIRST v5.0.0 http://fsl.fmrib.ox.ac.uk/fsl/fslwiki/FIRST) in FMRIB's Software Library (FSL, v5.0, http://fsl.fmrib.ox.ac.uk/fsl/fslwiki/) was used to measure hippocampal volume and morphometry; (3) the longitudinal pipeline in FreeSurfer (v5.1.0, http://freesurfer.net) was applied to measure the longitudinal training effect on cortical thickness on a vertex basis. Please refer to Supplementary Information for more details.

T2 fluid attenuated inversion recovery structure image. WMH volume is the main outcome of this MR modality. Regional WMH volumes were extracted using an in-house automatic pipeline that has been published elsewhere.
The outputs included total WMH volume across whole brain, and regional WMH volume of 18 white matter regions.

Resting-state fMRI preprocessing. The fMRI data were preprocessed using the SPM8-based (Statistical Parametric Mapping) Data Processing Assistant for Resting-State fMRI (DPARSF) tool-box (www.restfmri.net/) based on published protocols. In brief, this involved: discarding the first 10 volumes of each participant, slice timing, normalization to standard MNI space, resampling into 2 × 2 × 2 mm³ isotropic voxels, smoothing using a 8-mm kernel, removal of global signal trends, bypass filtering of 0.01–0.08 Hz and finally regressing out nuisance signals related to white matter, whole-brain and cerebrospinal fluid signal as well as 6 coregistration factors.

Seed-wise functional connectivity maps were then generated individually using Resting-State fMRI Data Analysis Toolkit (REST, www.restfmri.net). Bilateral hippocampal masks were selected as seeds from the Anatomical Automatic Labeling (AAL) template. The PC seed was obtained by thresholding a typical Default Mode Network generated using Independent Component Analysis (ICA) toolbox (Group ICA Toolbox GIFT, http://mialab.mrn.org/software/gift/) across whole baseline resting-state fMRI data. Individual functional connectivity (FC) maps for the hippocampal seed and PC seed were then generated based on correlations between the mean signal time course within each seed region and the rest of the brain.

Hippocampal surface-based MR statistical analyses. We used this postprocessing method to test longitudinal effects on morphometry of hippocampal surfaces generated by FIRST. The GLM design is identical with the voxel-based statistical design above, but implemented on FSL. The correction method we used here is the permutation test (n = 1000).

Vertex-based MR statistical analysis. Vertex-based analyses were used for cortical thickness (FreeSurfer) outputs. First, the change (rate) of cortical thickness that is defined by \((\text{thickness}_{\text{time}2} - \text{thickness}_{\text{time}1})/\text{years between two scans}\). Second, GLMs were designed as per the voxel-based statistical design above, but without the factor of time (as thickness change was the dependent variable) and subject (this is redundant). The covariates were also age, sex and education years. Finally, the multiple comparison error was corrected using whole-brain vertex-based FDR correction or small-volume-based FDR correction. Two prespecified areas were chosen a priori for small-volume correction: posterior cingulate cortex and medial temporal lobe.
Statistical analyses
Clinical outcomes and all region-of-interest-based MR outcomes were analyzed using a linear mixed model in SPSS (IBM, Armonk, NY, USA. Release 2012). This model was designed with three main effects (time, COG and RES), three interactions (COG×time, RES×time and COG×RES×time) and three covariates (age, sex and education years). Mixed models are realistic and flexible with respect to possible variance differences between groups and over time and incorporate a model for missing values; all such analyses are therefore intention to treat. A compound symmetry model was used for repeat covariance. Pearson’s correlation was used to test the linkage between MR outcomes and cognitive outcomes across entire cohort. For mediation effect, Sobel tests were performed using the algorithm of Preacher and Hayes.70

RESULTS
Cognitive outcomes
We first focus on therapeutic benefits on cognition immediately at the end of training (6 months). A thorough report of cognitive SMART outcomes at the end of 18-month longitudinal follow-up is available elsewhere.58 Participants in any resistance exercise group (RES factor, see Figure 1b) improved on our primary outcome, the Alzheimer’s Disease Assessment Scale-Cognitive scale (ADAS-Cog), compared with non-RES groups (RES×TIME intention-to-treat mixed linear model, F(90) = 4.1, P < 0.05 Figure 1c), but not on the composite Memory Domain score. Conversely, those in any CCT group (COG factor, see Figure 1b) experienced no decline in Memory Domain scores observed in non-CCT groups (COG×TIME intention-to-treat mixed linear model, F(73) = 11.1, *P = 0.0017). (c) Enhancement of PC cortical thickness is correlated with improvement in global cognition (r = 0.25, P = 0.030, N = 75, Y axis reversed). Error bars represent 95% confidence interval. All group-based analyses controlled for age, sex and education. ADAS-Cog, Alzheimer’s Disease Assessment Scale-Cognitive scale; CCT, computerized cognitive training; PRT, progressive resistance training; RES, progressive resistant training factor.

Structural mechanisms
Training-induced cortical thickness change was evaluated with Freesurfer without any findings surviving whole-brain correction. However, two prespecified regions were examined in more detail.

Figure 2. (a) Significant RES×TIME interaction was found in the posterior cingulate (PC). Green shows definition of our prespecified region of interest (ROI), and red shows suprathreshold voxels following small-volume correction (*P < 0.05, T = 3.24, kv = 153 [−5 − 21 42]). (b) After extraction of individuals’ PC cortical thickness change (mm per year), participants in any PRT group displayed cortical expansion and less atrophy than those in non-PRT groups (RES×TIME, F(73) = 11.1, *P = 0.0017). (c) Enhancement of PC cortical thickness is correlated with improvement in global cognition (r = 0.25, P = 0.030, N = 75, Y axis reversed). Error bars represent 95% confidence interval. All group-based analyses controlled for age, sex and education. ADAS-Cog, Alzheimer’s Disease Assessment Scale-Cognitive scale; CCT, computerized cognitive training; PRT, progressive resistance training; RES, progressive resistant training factor.
using region-of-interest analyses, hippocampus and posterior cingulate cortex. A significant RES × TIME interaction was found in the PC (Figure 2a, $P_{\text{uncorrected}} < 0.05, T = 3.24, k^v = 153, [-5 - 21 42]$). On the basis of extracted PC measures, it is clear that PRT protected individuals from atrophy: PC cortical thickness increased by an average of 0.01 mm per year (± s.d. = 0.088) in PRT groups but decreased by an average of 0.05 mm per year (±0.085) in non-PRT groups ($F(73) = 11.1, P = 0.0017$, Figure 2b). When examined in more detail, combined PRT+CCT led to an expansion of cortical thickness and averted any atrophy in the PRT+SHAM group (Figure 2b). Therapeutic relevance was also supported given change in PC gray matter correlated with improvement in the trial’s primary outcome measure of global cognition, ADAS-Cog ($r = -0.25, P = 0.030, N = 75$). A formal Sobel test with bootstrap estimation showed that change in PC thickness tended to mediate improvement in global cognition (indirect mediation mean estimated value $-0.325, 95\%$ confidence interval $-0.914$ to 0.013).

Given the importance of hippocampal atrophy in AD, we used two complementary methods to assess for possible structural plasticity: manual delineation (blinded to time point and group) (Figure 3a) and automated morphological shape analysis using the FSL-FIRST procedure as implemented in a prior report of aerobic exercise. No significant interactions were observed on hippocampal volume or shape using either of these methods (Figures 3b–d).

Next, WMH volumes were analyzed at the whole-brain level as well as by major vascular territory as previously published by our group (Figure 4a). A near-significant trend was found for the RES × TIME interaction at the whole-brain level (log transformed, $F(75) = 2.8, P = 0.09$, Figure 4b), significant when analyzed at the regional level in the right periventricular zone ($F(75) = 4.3, P = 0.042$, Figure 4c) and right parietal zone ($F(75) = 4.1, P = 0.046$). In the right periventricular zone, WMHs regressed by 3.4% (±15.5%) over time in PRT groups but progressed by 3.0% (±15.9%) in non-PRT groups. Change in WMHs was not however linked to change in either ADAS-Cog or Memory Domain.

Functional mechanisms
Resting-state fMRI analysis focused on FC networks generated from two prespecified seeds: bilateral hippocampi and the PC (all results whole-brain corrected by false discovery rate). Complex training-induced changes were observed for each FC network (see Figure 5, as well as Supplementary Information).
For PCFC, RES × TIME effects were found indicative of decreased connectivity with the left inferior temporal lobe \(F(67) = 14.8, P < 0.001\), Supplementary Information as well as the anterior cingulate cortex \(F(67) = 23.3, P < 0.001\), Figures 5a–c). COG × TIME analysis also indicated decreased connectivity with the left superior frontal lobe \(F(67) = 31.7, P < 0.001\); Supplementary Information) and anterior cingulate cortex \(F(67) = 13.9, P < 0.001\); Supplementary Information). Furthermore, a unique RES × COG × TIME interaction was found for the combined intervention in comparison with either stand-alone training, characterized by strongly decreased connectivity between the PC and anterior cingulate cortex \(F(65) = 5.3, P = 0.017\), see further results in Supplementary Information).

Analysis of the HIP FC network found RES × TIME effects suggestive of increased connectivity with the right middle frontal lobe \(F(67) = 13.0, P = 0.001\), Supplementary Information), but decreased connectivity with the right inferior temporal lobe \(F(67) = 18, P < 0.001\), Supplementary Information). COG × TIME analysis found evidence for increased connectivity between the hippocampus and left superior frontal lobe \(P = 0.012\), Figures 5e–g). In terms of therapeutic relevance, of all FC changes noted, it was only this strengthening of hippocampal functional connectivity that correlated with improved memory domain performance \(r = 0.33, P = 0.005\, N = 72\) and compare Figure 5h with Figure 5d). Furthermore, Sobel test found that strengthening of hippocampal–superior frontal connectivity mediated improvement in overall memory ability (indirect mediation mean estimated value 0.093, 95% confidence interval 0.006–0.215).

Finally, a unique RES × COG × TIME interaction was found for increased hippocampal–anterior cingulate cortex connectivity \(F(66) = 4.6, P = 0.005\), Supplementary Information) as well as increased hippocampal–right superior frontal lobe connectivity \(F(65) = 7.0, P < 0.001\), Supplementary Information) in the combined training condition compared with stand-alone training.

### DISCUSSION

Here we report for the first time that resistance training can conserve and even increase cortical thickness in the posterior cingulate. This mechanism may be salient to long-term protection from further cognitive decline and impairment because loss of PC gray matter is a biomarker of AD,71,72 most likely because of neuronal loss in specific cortical laminae.73,74 Furthermore, we found that individual variability in PC plasticity was correlated to improvement on the trial’s primary outcome, the ADAS-Cog. Previously, we have shown that resistance training improves the chances of categorical improvement on ADAS-Cog from impaired to nonimpaired,38 and hence this newly described mechanism is therapeutically relevant and unique to PRT as it is not induced by CCT. Accordingly, our data suggest that PRT can help improve global cognition in older individuals at risk for dementia by attenuating and perhaps reversing a salient AD process.
No evidence was found for structural plasticity in the hippocampus subsequent to either type of training. This is consistent with null MRI findings following memory training alone but is inconsistent with a previous report following long-term aerobic exercise. Because we replicated that study's image-processing pipeline, technical differences do not readily explain this discrepancy. Rather, it is possible that aerobic and resistance training produces distinct patterns of structural plasticity in older individuals. Evidence for structural plasticity in the rodent hippocampus almost invariably derives from aerobic voluntary wheel running—to date, there are no comparable animal data about the structural brain effects of resistance exercise. Exercise
Overall, the SMART trial shows that resistance and cognitive training can be used to target different cognitive domains based on distinct brain mechanisms relevant to aging, cerebrovascular disease and AD. Given the alarming disease burden predicted for dementia and neurocognitive disorders over the coming decades, this information should help design more effective dementia prevention trials as well as contribute to their clinical and community implementation.

**CONFLICT OF INTEREST**

The authors declare no conflict of interest. MJV has previously received honoraria for speaking at Pfizer and The Brain Department LLC-sponsored events, has received research funding from The Brain Department LLC for unrelated work and currently receives in-kind research support in the form of no-cost software from BrainTrain Inc (USA) and in-kind research support from NeuroNation for unrelated projects. HB has been an investigator for Pfizer, Novartis, Janssen, Lilly, Medivation, Sanofi and Servier; a sponsored speaker for Pfizer, Novartis, Janssen and Lundbeck; and is on advisory Boards for Pfizer, Novartis, Janssen, Lundbeck, Merck and Baxter. BTB is a member of advisory boards and/or gave presentations for the following companies, for which he received honoraria: AstraZeneca, Lundbeck, Pfizer, Servier and Wyeth. NG holds shares in HeadStrong Brain LLC. New York although no dividends, gifts or royalties have ever been received and no work has been conducted for the company since 2007.

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