Sleep decreases neuronal activity control of microglial dynamics in mice

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Microglia, the brain-resident immune cells, are highly ramified with dynamic processes transiently contacting synapses. These contacts have been reported to be activity-dependent, but this has not been thoroughly studied yet, especially in physiological conditions. Here we investigate neuron-microglia contacts and microglia morphodynamics in mice in an activity-dependent context such as the vigilance states. We report that microglial morphodynamics and microglia-spine contacts are regulated by spontaneous and evoked neuronal activity. We also found that sleep modulates microglial morphodynamics through Cx3cr1 signaling. At the synaptic level, microglial processes are attracted towards active spines during wake, and this relationship is hindered during sleep. Finally, microglial contact increases spine activity, mainly during NREM sleep. Altogether, these results indicate that microglial function at synapses is dependent on neuronal activity and the vigilance states, providing evidence that microglia could be important for synaptic homeostasis and plasticity.
concentrations that may impact microglial morphodynamics\textsuperscript{24,27}. Despite evidence for microglial sensing of neuronal activity and synaptic pruning in physiological conditions, the impact of the sleep-wake cycle on microglial dynamics and functional properties has not been elucidated yet. In awake mice, noradrenergic tone was recently found to suppress microglial process area and surveillance territory when compared to anesthetized mice, but a clear description of the microglial process dynamics during sleep and the underlying regulation is lacking. Although the exact function of sleep is still elusive, there is a strong consensus as to its role in synaptic homeostasis and plasticity. Indeed, sleep and wake are important for learning and memory consolidation and are associated with molecular mechanisms of synaptic plasticity that may involve microglial cells\textsuperscript{28,29}.

To better understand microglial morphodynamics in physiological conditions at the network and synaptic level, we combined electrophysiological recordings in vigil head-restrained mice with two-photon in vivo imaging of microglial cells and neuronal activity. Our results show that global microglial motility and complexity are overall correlated with changes in neuronal activity and that change in activity at the spine level impacts the proximity and contacts of microglial processes with synapses. These relationships between neuronal activity and microglia morphodynamics were also found during the alternation of wake and sleep and are dependent on Cx3cr1 signaling. At a single-spine level, microglial processes are attracted towards active spines during wake, whereas microglial proximity and contact with spines are downregulated during NREM sleep, in a state-dependent manner. Finally, we found that microglial contact with spines resulted in an increase in spine activity which was mainly observed during NREM sleep.

Results

Microglial morphodynamics and microglia-spine contacts are modulated by spontaneous neuronal activity

Microglia are constantly surveying the brain parenchyma, and changes in neuronal activity may impact their morphodynamics. However, the influence of neuronal network activity is not completely understood. For this reason, we assessed microglial morphodynamics in the somatosensory cortex of Cx3cr1\textsuperscript{1-}\textsuperscript{t}\textsuperscript{m} mice using two-photon microscopy while simultaneously monitoring brain activity with electroencephalogram (EEG) recordings (Fig. 1a). To this aim, we concurrently performed thinned-skull cortical window preparation and electroencephalogram (EEG)/electromyogram (EMG) electrode implantation (Fig. 1b). Brain activity was recorded and monitored during the 30–35 min of the imaging sessions. The activity was characterized by periods of high- and low-amplitude activity (Supplementary Fig. 2a).

To study the relationship between microglial morphodynamics (Fig. 1c) and neuronal activity, we first performed the cross-correlation between microglial complexity (ramification) and EEG power, as well as the cross-correlation between motility (dynamics) and EEG power. We found that both microglial complexity (Fig. 1d) and motility (Fig. 1e) were negatively cross-correlated with the EEG power, suggesting that high-amplitude activity is linked to lower microglial morphodynamics and vice versa. This result suggests that microglial morphodynamics could be driven by global cortical activity. To assess this hypothesis, we calculated the correlation between the motility and complexity of pairs of microglial cells as a function of their interdistance (Supplementary Fig. 2b). Our rationale was as follows: when microglial morphodynamics is synchronized for several microglial cells in our field of view (200 x 200 \( \mu m \)), this suggests a global impact of neuronal activity. On the other hand, if individual microglia behave independently from each other, a local regulation of motility and complexity might be conceivable. We found that the complexity changes between microglial cells are correlated (Fig. 1f), even though the correlation slightly decreases with the distance, from 0.84 when microglia are at a distance of 42 \( \mu m \) from each other to 0.25 when separated from 98 \( \mu m \). This result indicates that complexity might reflect a dependency on global brain activity. On the other hand, motility changes were weakly correlated with the EEG power, and the correlation strongly decreases when the distance between microglia increases (Fig. 1g) from 0.72 when microglia are at a distance of 42 \( \mu m \) from each other to ~0.31 when microglia are at a distance of 98 \( \mu m \) (Supplementary Fig. 2b). These results suggest that the regulation of microglial complexity and microglial motility originate from different levels of integration. While complexity seems to respond to global neuronal activity, motility rather depends on the local network, possibly at the synaptic level.

Previous studies have found that microglial processes are in close proximity with spines, and that this relationship may be activity-dependent\textsuperscript{24,28}. To study microglial dynamics at the synaptic level, we simultaneously recorded microglial cells in Cx3cr1\textsuperscript{CreERT2}\textsuperscript{t} Rosa26-STOP-tdTomato\textsuperscript{m} mice, expressing the reporter gene tdTomato in microglia, and fluctuations of intracellular Ca\textsuperscript{2+} concentration as a proxy of neuronal activity at the dendritic spine level after GCaMP6 injection (Fig. 1b). We found that microglial processes make frequent contacts with dendritic spines (Fig. 2a) lasting on average ~4.38 min ± 0.42 (Supplementary Fig. 2c). Active spines were contacted on average ~35% of the time by microglial processes, even though contact duration was highly variable (Supplementary Fig. 2d).

To assess whether local spine activity affects microglia-spine interaction, we studied the correlation between the activity of the spine and the duration of microglia-spine contact. We found that this correlation was positive and that microglial processes stayed longer in contact with highly active spines (Fig. 2b, Pearson correlation test, \( p < 0.05 \)). To test whether this profile may be observed by a random distribution of values for contact duration and spine activity, we performed the same analysis with scrambled original data. We did not find any correlation for this random data set (Fig. 2c, Pearson’s correlation test, \( p > 0.05 \)), indicating that microglial contact with spines is activity-dependent.

Modulation of neuronal activity by whisker stimulations changes microglial process proximity and contacts with spines

To strengthen our observations and provide a causal evidence of the relationship between microglial dynamics and neuronal activity, we decided to modulate neuronal activity by stimulating the C2 whisker (Fig. 3a) while monitoring spine activity (Fig. 3b) and microglial processes in the corresponding contralateral barrel. We first ensured that the repetition of stimulations (1 s stimulation at 90 Hz every 30 s during 25 min) did not induce synaptic plasticity of the network (Supplementary Fig. 3a, one-way ANOVA, \( p > 0.05 \)). Because of the polysynaptic nature of the network, we found that stimulations of the whisker induced three different types of response (Supplementary Fig. 3b), 39.3% of the spines studied responded by an increase of activity (Fig. 3c–e, unpaired \( t \)-test, \( **p < 0.0001; e, \text{paired} \ t\text{-test, two-tailed,} \ **p < 0.0001 \)), 24.9% of spines by a decrease of activity (Fig. 3c, d, f, unpaired \( t \)-test, \( **p < 0.0001; f, \text{paired} \ t\text{-test, two-tailed,} \ **p < 0.0001 \)) while 35.8% of spines did not respond significantly to whisker stimulations (Supplementary Fig. 3c, d, one-way ANOVA, \( **p < 0.0001; d, \text{paired} \ t\text{-test, two-tailed,} \ p > 0.05 \)). We found that the contact duration between microglial processes and spines was longer for the responding spines compared to decreased activity spines during stimulations (Fig. 3g, unpaired \( t \)-test, \( p < 0.05 \)) while not being different during baseline (Supplementary Fig. 3e, unpaired \( t \)-test, \( p > 0.05 \)). For the 147 spines that responded by an increased activity we found that the proportion of spines contacted by a microglial process at a given time increased by 7.9 ± 3.2 % after 10–15 min stimulation when compared to baseline (Fig. 3h, one-way ANOVA, \( p < 0.05 \)) and the spines spent on average 12.7 ± 4.4 % more time after 10–15 min of whisker stimulations (Fig. 3i, one-way ANOVA, \( p < 0.05 \ **p < 0.001 \)). On the contrary, for the 93 spines that exhibited a decreased activity
Fig. 1 | Neuronal activity correlates with microglial complexity and motility. 

a, b Schematic representation of our experimental setup. a Head-restrained mice were trained for simultaneous two-photon imaging with electrophysiology (side view). b Fronto-parietal EEG and neck EMG electrodes were implanted, combined with a thinned-skull cortical window preparation and calcium indicator injection (top view). c Example of microglial motility over a 5-min period, showing microglial process retractions in magenta, and process extensions in cyan. Scale bar = 10 μm. Cross-correlation analysis between d microglial complexity (n = 6 mice, 2–7 microglial cells/mouse) and e motility (n = 6 mice, 2–7 microglial cells/mouse) with EEG power. This experiment was repeated independently with similar results, as shown in Fig. 3h–i. Distribution of the correlation coefficient of the f complexity (n = 3–4 pairs of microglial cells per mouse) and g motility (n = 3–4 pairs of microglial cells per mouse) for pairs of microglial cells as a function of their distance. Source data are provided as a Source Data file for d–g.
Fig. 2 | Microglia contact spines in an activity-dependent manner.
a Simultaneous imaging of microglial processes (magenta, arrow) and neuronal GCaMP6 expression (cyan) in the L1 of the primary somatosensory cortex. The arrowheads indicate contacts between microglial processes and spines. The dynamic interactions between microglial processes and spines are shown in a smaller FOV (delimited by the white square) over a 10 min period. Examples of microglial processes interacting with spines are indicated with the white arrowheads, whereas spines not in contact with microglia are pointed with white arrows. The brightness and contrast were adjusted for visualization purposes. One representative image with ten replicates. 
b Correlation between Ca²⁺ spine frequency and the duration of microglia-spine contact (n = 68 spines from five mice. Pearson’s correlation test, two-tailed, p = 0.012). 
c Correlation between spine activity and duration of microglia-spine contact for a random data set (n = 68 spines from five mice, Pearson’s correlation test, two-tailed, p = 0.42). All data are represented as mean ± SEM. Source data are provided as a Source Data file for b, c.

during simulations, we found that the proportion of spines in contact during stimulation (Fig. 3l, one-way ANOVA, *p < 0.05) as well as the percentage of time that spines spent in contact with microglial processes decreased by 11.2 ± 4.8% and 13.3 ± 5.8%, respectively 10–15 min following the onset of the stimulation (Fig. 3k, one-way ANOVA, *p < 0.05). Finally, when measuring the relative distance of the closest microglial process with respect to spines, we found that microglial processes were closer during stimulation for spines that responded by an increase of activity and further away during stimulation for spines that responded by a decrease of activity (Fig. 3l, Kolmogorov-Smirnov test, **p < 0.01), while no difference was observed between the groups during the baseline period (Supplementary Fig. 3f, Kolmogorov-Smirnov test, p > 0.05). It is interesting to note that for spines which did not exhibit a response to the stimulations, no change was observed in the proportion of spines being contacted, the percentage of time spent in contact, and the distance between the closest microglial process and the spine (Supplementary Fig. 3g–i, one-way ANOVA, p > 0.05; h, one-way ANOVA, p > 0.05; i, Kolmogorov-Smirnov test, p > 0.05). Altogether these results indicate that modulation of neuronal activity induces changes in the proximity of microglial processes with respect to spines, the proportion of spines being contacted by a microglial process, and the contact duration.

Vigilance states influence microglial morphodynamics and microglia-spine interaction

The vigilance states are physiological conditions during which activity is drastically changing. To examine whether microglial complexity and motility are influenced by the change of neuronal activity associated with the vigilance states, we performed two-photon imaging of microglial cells while simultaneously scoring the vigilance states through EEG and EMG recordings. Each session included several episodes of wake and NREM sleep (Fig. 4a, b) during which microglial morphodynamics varied (Supplementary Fig. 4a, b). The same microglial cell imaged during wake and NREM sleep displayed higher motility and complexity (wake in magenta and sleep in cyan) during wake compared to NREM sleep (Fig. 4c and Supplementary Fig. 4c). Quantifications of microglial morphology and motility in vivo revealed that microglial complexity (Fig. 4d, Wilcoxon test, *p < 0.05) and motility (Fig. 4e, Wilcoxon test, **p < 0.05) were significantly reduced during NREM sleep compared to wake. Of note, the average proportions of NREM sleep and wake were comparable for the recordings chosen for analysis (Supplementary Fig. 4d, Wilcoxon test, p > 0.05), and one episode of a given vigilance state lasted on average 5.86 min ± 0.46. Further details about the characteristics of the sleep-wake episodes in our recordings can be found in Supplementary Figs. 4e–l.

These results indicate that microglia are sensing the vigilance states, possibly through the change of neuronal activity associated with a given vigilance state, and adapt their morphodynamics accordingly.
Fig. 3 | Modulation of neuronal activity by whisker stimulation controls microglial dynamics towards dendritic spines. a Experimental set-up: Contralateral single whisker stimulation (90 Hz, 1 s) every 30 s, relative to the imaging location in the corresponding somatosensory barrel cortex in Cx3cr1CreERT2+/ROSA26-STOP-tdGreen mice transduced with AAV1.Syn.GCaMP6m. b Example of one image from 9 replicates, showing maximum intensity time and Z-projections of the Ca2+ signal (35 minutes, 14 planes, 1 µm/plane) used for spine selection. Scale bar=10 µm. Brightness and contrast were adjusted for visualization purposes. c Normalized color-coded calcium activity of a set of 15 individual spines shown in b, categorized as Increased and Decreased activity spines. d Average success rate of individual spines in response to the stimulations \((n_{DA} = 147\) spines and \(n_{IA} = 93\) spines from three mice, unpaired t-test, two-tailed, \(*p < 0.0001\)). Average spontaneous frequency of Ca2+ events for individual spines plotted before and during the stimulation period for e Increased activity spines \((n_{IA} = 147\) spines from three mice, paired t-test, two-tailed, \(*p < 0.0001\) and f Decreased activity spines \((n_{DA} = 93\) spines from three mice, paired t-test, two-tailed, \(*p < 0.0001\)). g Average duration of microgial-spine contact during the stimulations \((n_{IA} = 141\) contacts and \(n_{DA} = 57\) contacts from three mice, unpaired t-test, two-tailed, \(*p = 0.028\)). h Kinetics of the proportion of spines contacted by microglial processes for Increased activity spines \((n_{IA} = 147\) spines from three mice, one-way ANOVA, \(*p = 0.048\) and I Average percentage of time individual spines spent in contact with microglial processes for Increased activity spines \((n_{IA} = 147\) spines from three mice, one-way ANOVA, \(*p = 0.0396\), \(*p = 0.0063\), \(*p = 0.0394\) and \(*p = 0.0133\)). j Kinetics of the proportion of spines contacted by microglial processes for Decreased activity spines \((n_{DA} = 93\) spines from three mice, one-way ANOVA, \(*p = 0.0255\) and \(*p = 0.02\)) and k Average percentage of time individual spines spent in contact with microglial processes for Decreased activity spines \((n_{DA} = 93\) spines from three mice, one-way ANOVA, \(*p = 0.027\), \(*p = 0.018\), \(*p = 0.0206\), \(*p = 0.0479\) and \(*p = 0.0451\)). Cumulative probability of the distance to the closest microglial process during a 5-min episode during the stimulation period \((n_{IA} = 147\) spines and \(n_{DA} = 93\) spines from three mice, Kolmogorov-Smirnov test, \(*p = 0.002\)). All data are represented as mean ± SEM. Source data are provided as a Source Data file for d–l.

Fig. 4 | Microglial morphodynamics is modulated by the vigilance states. Representative EEG and EMG traces during a wake and b sleep. c A color-coded image showing microglial complexity during wake (in magenta) and during sleep (in cyan). Scale bar=10 µm. Quantification of d microglial complexity \((n = 6\) mice, 3–7 microglial cells/mouse, Wilcoxon test, two-tailed, \(*p = 0.0313\)) and e motility morphodynamics associated with the vigilance states. Because the deletion of the Cx3cr1 gene in microglia could alter the quality of sleep, we analyzed and compared sleep episodes between Cx3cr1−/− and Cx3cr1−/+ mice. Overall, the percentage of time spent in NREM sleep, the duration, and the number of NREM sleep episodes were not significantly different between groups (Fig. 5d–f, Mann-Whitney test, \(*p < 0.05\)). Another possibility explaining the absence of motility change in homozygous mice could be that the neuronal activity differs from the one monitored in heterozygous mice. To test that hypothesis, we compared the EEG power spectrum of Cx3cr1−/− and Cx3cr1−/+ mice and found no differences in the amplitude-frequency plots (Fig. 5g, unpaired t-test, two-tailed, \(p > 0.05\)), indicating that global cortical activity was similar between Cx3cr1−/− and Cx3cr1−/+ mice. Finally, we looked at the cross-correlation between EEG power and microglial complexity or
motility and we found that the correlation was weaker in Cx3cr1<sup>−/−</sup> when compared to Cx3cr1<sup>+/−</sup> mice (Fig. 5h, i, Wilcoxon test, *p < 0.05). This indicates that the relationship between neuronal activity and microglial morphodynamics is lost when the Cx3cr1 receptor is absent. Altogether these results indicate that the Cx3cr1 signaling is important in the regulation of microglial cells’ morphodynamics with regards to neuronal activity.
NREM sleep limits the attraction of microglial processes toward active spines

Since microglial processes appear to sense neuronal activity and are attracted toward active spines, we wanted to assess whether this attraction may be influenced by the vigilance states. We first found that the frequency of spine activity is not significantly different during wake and NREM sleep (Supplementary Fig. 5a, paired t-test, two-tailed, p > 0.05, Supplementary Fig. 5b for results per mice). Microglial processes appeared closer to spines and their contact duration with spines was longer during episodes of wake when compared to sleep (Fig. 6a).
We then quantified the proportion of spines in contact with microglial processes during wake and NREM sleep, and found no significant difference (Fig. 6b, Wilcoxon test, \( p > 0.05 \)). However, by investigating the distribution of microglial processes around spines during the different vigilance states, we found that microglial processes were closer to spines during wake (Fig. 6c, Kolmogorov–Smirnov test, \( ***p < 0.0001 \)). Furthermore, microglial processes spent slightly more time in contact with spines during wake when compared to NREM sleep (Fig. 6d, paired \( t \)-test, two-tailed, \( p < 0.05 \), Supplementary Fig. 5c for results per mouse), indicating an important influence of NREM sleep on microglia–spine interactions.

Having observed the impact of NREM sleep on the global distribution of processes and duration of microglia–spine contacts, we next wanted to evaluate more precisely the effect of NREM sleep on the positive attraction of microglial processes towards active spines. For this reason, we studied microglia–spine interactions in various regimens of synaptic activity during the vigilance states. We classified spines into three categories: spines mostly active during wake, spines mostly active during NREM sleep, and spines with balanced activity between NREM sleep and wake (Supplementary Fig. 1b), and we were interested in spines that exhibited most activity during one of the vigilance states. We studied the proximity of microglial processes with regards to spines mostly active during wake or during NREM sleep, and the duration of microglia–spine contact. We found that microglial processes were closer to spines active during wake (Fig. 6e, f, Kolmogorov–Smirnov test, \( ***p < 0.0001 \)). This observation holds true whatever the vigilance state during which the contact was monitored (Fig. 6g, h, Kolmogorov–Smirnov test, \( ***p < 0.0001 \)). Furthermore, microglial processes were closer during wake both for spines mostly active during wake and spines mostly active during NREM sleep, suggesting that this relationship is impeded during NREM sleep (Supplementary Fig. 5b, c, Kolmogorov–Smirnov test, \( ***p < 0.0001 \)). Spine activity was well correlated with microglia–spine contact duration for spines active during wake, but not as well for spines active during NREM sleep (Fig. 6i, j, Pearson’s correlation test, \( **p < 0.01 \)). In addition, the contact duration was reduced during NREM sleep for spines active during wake (Fig. 6k, paired \( t \)-test, two-tailed, \( p < 0.05 \), Supplementary Fig. 5f for results per mouse). This was not detected for spines active during NREM sleep (Fig. 6l, paired \( t \)-test, two-tailed, \( p > 0.05 \), Supplementary Fig. 5g for results per mouse).

**Microglial contact induces spine activity increase during NREM sleep**

Since microglial contact was recently found to increase spine activity\(^9\), we wanted to assess whether this increase in activity may occur in both states or is vigilance state-dependent. By quantifying spine Ca\(^{2+}\) transients without and during contact with microglial processes, we confirmed that overall spine activity was significantly
increased during contact with microglial processes without considering the vigilance state (Fig. 7a, b, b, paired t-test, *p < 0.05, Supplementary Fig. 5h for results per mice). Intriguingly, during contact, the increase in spine activity was significantly higher during NREM sleep compared to wake (Fig. 7c, one-way ANOVA, *p < 0.05, Supplementary Fig. 5i for results per mice), indicating that the contact-induced increase in activity may be vigilance state-dependent, mainly occurring during NREM sleep.

Discussion

In this work, we investigated the impact of neuronal activity and vigilance states on microglial dynamics at the network and the synaptic level. We report that neuronal activity largely contributes to changes in microglial morphodynamics. This was observed when monitoring spontaneous neuronal activity, as well as when neuronal activity was modulated by physiological stimulations. We also found that microglial morphodynamics was modulated by the vigilance states, likely mediated by the changes in neuronal activity, through a signaling pathway involving Cx3cr1. Microglial morphology was globally following the changes of neuronal activity associated with the vigilance states, whereas motility was likely regulated at the synaptic level. Finally, microglial contact increased spine activity, mostly during NREM sleep.

In physiological conditions, microglial processes are highly ramified and dynamic, continuously surveying the surrounding parenchyma, but their regulation remains poorly understood. By concurrently monitoring microglial morphodynamics and the electrical activity of the brain in vigilant mice, we found that EEG power was negatively cross-correlated with microglial morphodynamics, linking neuronal activity patterns to microglial morphodynamics (Fig. 1d,e). High EEG power, reminiscent of synchronized activity and slow-wave dominated state, may be observed after administration of certain anesthetics, such as ketamine/xylazine or fentanyl cocktail. Several studies have assessed their impact on microglial morphodynamics, but results have been inconclusive, possibly due to differences in methodology, brain region studied, and quantification of morphodynamics parameters. In a previous study, we found that ketamine/xylazine, dominated by high-amplitude, low-frequency oscillations, led to a reduction in microglial morphodynamics, suggesting important regulation of microglial morphology by the patterns of neuronal activity. An interesting question arising from this finding is whether the temporal evolution of microglial morphodynamics is comparable between microglial cells or is intrinsic to each cell. Changes in morphology were highly correlated for microglial cells (<120 µm apart), suggesting a global impact of neuronal activity on microglial morphology and its degree of ramification. On the other hand, motility changes were not as well correlated between microglial cells, indicating that motility could be regulated at the local level. Indeed, spontaneously active neurons, HFS, or trains of AP in a single neuron may recruit microglial processes potentially at the synaptic level. In our study, we found that microglial processes spent more time in contact with spines displaying high Ca²⁺ transient frequencies (Figs. 2, 3). This observation was true for spontaneous activity or when the network was recruited by a high noradrenergic tone. Moreover, the results described in the current study are obtained using a thinned-skull preparation. It has also been shown recently that noradrenaline is high during NREM sleep especially during spindle episodes. These latest results indicate that it is difficult to speculate on the role of noradrenaline during vigilance states in absence of proper measurements of the noradrenaline tone during the alternation of wake and sleep in the cortex. The mechanisms driving microglia morphodynamics changes are still elusive and are likely diverse. Excitatory and inhibitory neurotransmitters (NTs) fluctuate at the cortical level during the vigilance states. Increase in ionotropic GABA transmission, found during sleep, resulted in significant reduction of microglial motility and morphology in retinal explants, which is in line with our results. During wake, among other NTs, cortical norepinephrine and serotonin are increased, but these have divergent effects on microglial cells. Norepinephrine caused microglial process retraction, whereas serotonin has chemotactic effect on microglial processes. Thus, the effect of the complex neuromodulatory environment of the sleep-wake cycles on microglial morphodynamics needs to be further assessed. Besides NTs, several ions exhibit state-dependent changes of concentration; for instance arousal is associated with a rapid rise in [K⁺]ₑ along with a slower decrease in [Ca²⁺]ₑ and [Mg²⁺]ₑ. Baseline microglial morphodynamics is regulated by changes in [K⁺]ₑ; however, the [K⁺]ₑ change required to induce microglial dynamics is far beyond the slight [K⁺]ₑ shift observed during the vigilance states. Therefore, changes occurring in the extracellular space during the vigilance states are multiple and the exact mechanisms influencing microglial morphodynamics remain to be determined.

Several studies have investigated the role of Cx3cr1 and various results were found depending on the area investigated. In the visual cortex, Cx3cr1 did not seem to be required for activity-dependent plasticity, while in the hippocampus Cx3cr1 was shown to be involved in synaptic functions. In our study, we explored the involvement of Cx3cr1 signaling in microglia-neuron communication (Fig. 5). Our results indicate that when the membrane Cx3cr1 receptor is absent, the change of morphodynamics associated with NREM sleep is largely decreased as well as the correlation between neuronal activity and microglial morphodynamics. This indicates that fractalkine released by neurons could be activity-dependent and constitutes an important signaling mechanism involved in the control of microglial morphodynamics by neurons. Interestingly, Cx3cr1 impairment did not affect...
the EEG spectrum nor the quantity of sleep in our mouse model of head restriction. It is important to note that the model we are using to invalidate Cx3cr1 consists in the insertion of eGFP in the cx3cr1 gene. This has two consequences. First, in heterozygous mice (Cx3cr1+−) that we used for our experiments, the quantity of Cx3cr1 is lower than in wild-type mice, which could impact the physiology of the mouse. Second, on Cx3cr1−/− mice, the expression of eGFP is twofold when compared to heterozygous mice. This has been taken into account when performing imaging as we reduced the laser power to reach an eGFP signal equivalent to the one measured in heterozygous mice. This increased expression of eGFP should not interfere with the effects we are reporting as we compared morphodynamics between wake and sleep within the same mouse.

Our study, along with several others, has provided evidence that microglial dynamics seems to be activity-dependent and microglial processes are attracted towards sites of increased activity46-48. Elucidating neuronal activity during sleep has been an open question for many years. Contrary to Ca2+ transients in the soma, when calcium dynamics are monitored at the dendritic level, the decrease in calcium activity was not observed during NREM sleep47. In a similar manner, our monitoring of calcium activity in spines indicates that the frequency of Ca2+ transients does not change between wake and NREM sleep at the spine level. Furthermore, NREM sleep is composed of different EEG rhythms: slow wave (0.5-4 Hz) and spindle-rich activity (9-16 Hz), that have profoundly different activity and possible impact on microglial cells. Even though we report decreased microglial morphodynamics during NREM sleep, the impact of the different stages of sleep may not be straightforward and needs to be assessed more closely in future studies using a better temporal resolution. Nonetheless, we found that microglial processes were overall closer to spines and spent more time in contact with spines active during wake (Fig. 6). The positive attraction was affected by NREM sleep as microglial processes were farther from spines and the correlation between spine activity and contact duration was reduced. Our findings suggest that microglial processes seem to sense neuronal activity predominantly during wake, and sleep might hinder this attraction. The exact mechanisms by which microglia-spine interactions differ during sleep and wake warrant further investigation and are beyond the scope of this paper, but a regulation of the expression of Cx3cr1 cannot be excluded as described in ref. 46.

Microglial contact with neuronal components has previously been found to increase local spine activity or homeostatically downregulate neuronal activity49-51. Like previously reported by Akiyoshi et al., we observed an increase in spine activity during contact with microglial processes (Fig. 7). The exact mechanisms remain unknown, but microglia may secrete many soluble molecules locally, such as cytokines, neurotrophic factors, and NT, capable of influencing neuronal activity46. They may also release extracellular vesicles that may increase glutamate release at presynaptic sites47 and trigger intracellular Ca2+ elevation by contact-dependent mechanism13. Unexpectedly, the increase in spine activity during microglial contact took place during sleep, and to our knowledge, this is the first report of microglia modulating spine activity in a specific vigilance state.

Since the function of sleep has been associated with synaptic homeostasis and memory, a tempting speculation would relate these specific contacts with synaptic scaling mechanisms. Two predominant theories of synaptic scaling during sleep are hotly debated. The active system consolidation theory proposes that sleep is involved in strengthening of synapses tagged during wake, by active replay during slow wave sleep. On the other hand, the synaptic homeostasis hypothesis suggests a global synaptic downsampling during sleep, which counters synaptic potentiation generated during wake. Even though microglia may be involved in both functions, our findings suggest that during sleep, microglia may be less oriented toward sensing neuronal activity, but potentially towards exerting specific functions at synapses, such as strengthening specific synapses.

Furthermore, Akiyoshi et al., suggested that microglia-dependent increase in spine activity may contribute to local network synchronization47. Taking into consideration that spindle-rich NREM sleep is associated with increased and synchronized activity in dendrites47, it is possible that microglia may participate in local dendritic spindle-related plasticity during sleep. Contrary to Akiyoshi et al., a brain-wide ablation of microglia led to increased neuronal synchronization in the striatum47, suggesting that the microglia-neuron interaction and functional consequences may be region-dependent. Bearing in mind these findings, future studies need to determine the temporal and spatial requirements for increased network synchronization caused by contact-dependent microglial increase in spine activity.

In conclusion, despite being the resident immune cells of the brain, recent studies attribute fundamental physiological functions to microglial cells, including contribution to synaptic connectivity and properties, as well as the regulation of neuronal activity and network. These newly discovered tasks depend on the integrity of microglial morphology and motility. We demonstrate that microglial motility and morphology are modulated during the vigilance states, both globally and at the level of the spine. Spine activity, and especially the vigilance state in which activity is occurring, impacts microglial proximity and contact with spines, resulting in functional consequences during contact. Based on our findings, we propose that microglial processes may sense neuronal activity particularly during wake and increase spine activity during sleep. These findings provide a basis for future work in understanding the mechanisms regulating microglial dynamics and microglia-spine activity across the vigilance states and excitingly, the potential functions of microglia in synaptic homeostasis. Understanding these mechanisms at the physiological level is crucial for understanding how sleep disruptions and microglial activation in pathological conditions may impact these processes.

Methods

Animals

Microglial motility and complexity imaging was performed in six to ten-week-old male Cx3cr1−/− mice that we refer to as Cx3cr1+/− in the text, that expressed enhanced green fluorescent protein (eGFP) under the control of the Cx3cr1 promoter13, while Cx3cr1−/−/ROSA26STOP-tdTomato+/− mice (Cx3cr1+/− in the text), in which Cx3cr1 was knocked out on both alleles, were used to image microglial morphodynamics when Cx3cr1 signaling is invalidated. For microglial dynamics and spine activity analysis, Cx3cr1CreERT2+/− mice were crossed with ROSA26STOP-tdTomato+/− mice, to generate Cx3cr1CreERT2+/− ROSA26-STOP-tdTomato+/− mice. All transgenic mice were 6 to 10-week-old males, derived from the C57BL/6 strain. Mice were housed in enriched and ventilated cages with bedding and running wheels, at 22 ± 2 °C under 12/12 h light/dark cycle (light onset at 7:00 a.m.) and were given access to food and water ad libitum at ALECS, SCAR, and ANIPHY Facilities. All animal procedures were conducted in accordance with the Guidelines of the Animal Care Facility of University Claude Bernard Lyon 1 and were approved by French Ministry of Agriculture (Apas #DR2014-14, Apas #7839, Apas #10350 and Apas #20983) and Local Ethics Committee CE2A55.

Induction of Cre activity with Tamoxifen treatment

Tamoxifen (catalog # T-5648; Sigma-Aldrich) was dissolved in warm sterile olive oil (catalog # B8017-25-0, Sigma Aldrich, warmed at 55°C) at a concentration of 20 mg/ml. Six to seven-week-old Cx3cr1CreERT2+/− ROSA26-STOP-tdTomato+/− mice were injected subcutaneously in the thigh at 0.4 mg/g, twice, 48 h apart.
Surgery and habituation
Mice were deeply anesthetized with isoflurane (3–4%, Isovet, Piramal Healthcare, UK Ltd.) and mounted in a stereotactic frame (D. Kopf Instruments). Isoflurane anesthesia was maintained at concentrations of 1–3% during the surgical procedure. To reduce postoperative pain and inflammation, we administered Carprofen (5 mg/kg s.c.) before surgery, and for two consecutive days following surgery. After the skull was thoroughly cleaned and exposed, two EEG screws were inserted in the frontal and parietal cortex of the right hemisphere and two EMG electrodes were inserted in the dorsal neck muscles. A custom-designed 0.5-mm diameter cranial implant was firmly glued on the left hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the somatosensory cortex using a high-speed dental drill until reaching 20–30 μm bone thickness. Most of the drilling was performed in cold, sterile saline solution which allowed continuous cooling and humidification of the bone to avoid heat-induced tissue injury, desiccation of the bone, and inflammation. To visualize Ca²⁺ dynamics in spines of L2/L3 pyramidal neurons of the somatosensory cortex, we performed a small craniotomy (300 μm) and injected 500–700 nl of AAV1.Syn.G-CaMP6m.WPRE.SV40 (UPenn Vector Core, designed 0.5-mm diameter cranial implant was
surgically placed for each animal. A cover glass was thoroughly cleaned and exposed, two EEG screws were inserted in the frontal and parietal cortex of the right hemisphere and two EMG electrodes were inserted in the dorsal neck muscles. A custom-designed 0.5-mm diameter cranial implant was firmly glued on the left hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the somatosensory cortex using a high-speed dental drill until reaching 20–30 μm bone thickness. Most of the drilling was performed in cold, sterile saline solution which allowed continuous cooling and humidification of the bone to avoid heat-induced tissue injury, desiccation of the bone, and inflammation. To visualize Ca²⁺ dynamics in spines of L2/L3 pyramidal neurons of the somatosensory cortex, we performed a small craniotomy (300 μm) and injected 500–700 nl of AAV1.Syn.G-CaMP6m.WPRE.SV40 (UPenn Vector Core, designed 0.5-mm diameter cranial implant was surgically placed for each animal. A cover glass was thoroughly cleaned and exposed, two EEG screws were inserted in the frontal and parietal cortex of the right hemisphere and two EMG electrodes were inserted in the dorsal neck muscles. A custom-designed 0.5-mm diameter cranial implant was firmly glued on the left hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the hemisphere using acrylic-based dental adhesive resin cement (Super bond; Sun Medical). The skull was carefully thinned over the somatosensory cortex using a high-speed dental drill until reaching 20–30 μm bone thickness. Most of the drilling was performed in cold, sterile saline solution which allowed continuous cooling and humidification of the bone to avoid heat-induced tissue injury, desiccation of the bone, and inflammation. To visualize Ca²⁺ dynamics in spines of L2/L3 pyramidal neurons of the somatosensory cortex, we performed a small craniotomy (300 μm) and injected 500–700 nl of AAV1.Syn.G-CaMP6m.WPRE.SV40 (UPenn Vector Core, in order to minimize tdTomato bleaching. Imaging was performed in the L1 of the C2 barrel cortex at a depth of 60–120 μm from the cortical surface because of higher spine density. The imaging area was 100 × 100 μm sampled on 256 × 256 pixels i.e., pixel size of 0.4 μm. Z-stacks containing 14–16 consecutive images were acquired every 7 s, with a step size of 1 μm/optical section. A typical recording lasted 35 min (300 Z-stacks).

For Microglial dynamics and calcium imaging experiments during whisker stimulation, 3D imaging of microglial dynamics was performed using two laser lines: a first laser line tuned to 1040 nm for excitation of the fluorescent protein tdTomato, and a second laser line tuned to 950 nm for excitation of the fluorescent protein eGFP. This configuration was chosen to minimize tdTomato bleaching. Imaging was performed in the L1 of the C2 barrel cortex at a depth of 60–120 μm from the cortical surface because of higher spine density. The imaging area was 100 × 100 μm sampled on 256 × 256 pixels i.e., pixel size of 0.4 μm. A resonant scanner and a 400 μm piezo controlling device allowed us to perform Z-stacks (14 planes) acquisitions every 3.4 s, with a step size of 1 μm/optical section. To partially compensate for the difference in temporal resolution, we acquired four Z-stacks of the activity channel for every Z-stack of the microglia channel. A typical recording lasted -35 min (650 Z-stacks). Baseline was imaged for 10 min, followed by a period of 25 min during which whisker stimulations were performed.

Whisker stimulations were performed using a piezoelectric blade (PL410.11 PI Ceramic®) driven by a home-made microcontroller device. Stimulations were triggered each 30 s and lasted for 1 s at a frequency of 90 Hz⁻¹. The C2 whisker was inserted into a glass pipette fixed to the piezo blade, and we made sure that the whisker was still in the glass pipette at the end of each imaging session. Contact durations were measured on contacts happening during the stimulation period. To take into account the contacts which lasted longer than the 20 min period of stimulation we kept the contacts which lasted during all the stimulation period and started before the onset of the stimulations.

Analysis
Image processing and analysis were performed using custom-written Matlab scripts and LabVIEW. Brightness and contrast, as well as intensity normalization and noise filtering were performed before 3D co-registration calculated by triple Fourier Transform. The microglial cell Z-stacks were then corrected for drift and movements in the x, y, and z planes during time-lapse image acquisition. Each volume was registered to the first volume chosen as reference. The shift measurement was obtained from volumes’ cross-correlation calculated by fast Fourier transform. When animal movements were too important for automated registration, the time points were removed from the analysis.

For analysis of microglial motility and complexity during wake and sleep experiments, we manually delimited and cropped regions of interest containing the totality of one microglial cell from the 200 × 200 μm field of view using ImageJ (National Institute of Mental Health, Bethesda USA). Standard deviation intensity projections from the Z-stacks were performed to generate 2D time-lapse movies. To assess the complexity of microglial cells during wake and sleep, we converted the projections into binary and calculated the Hausdorff fractal dimension for each time point. The Hausdorff dimension is a measure of roughness also called fractal dimension D. This measure corresponds to the slope of the log-log characteristic function, drawing the number of tiles of size ε needed to cover all the surface of the object of interest. To analyze microglial motility, we performed subtractions between two consecutive Z-stack projections. For
visualization purposes, the lost and gained pixels between two consecutive time steps were pseudo-colored in magenta and cyan respectively, resulting in images where magenta and cyan points represented lost and newly formed processes, respectively. The total number of pixels of the absolute difference of two consecutive images determined the global motility coefficient (arbitrary unit).

During the deconvolution range of values for these parameters, after subtracting the median of the data for each cell, the cells were normalized for each parameter to fit a scale from +100 to −100. Thus, the data are all in the same range and their dynamics are comparable. Microglial complexity and motility index during wake and sleep were obtained by averaging the normalized values during wake and sleep for each imaging session.

For analysis of microglial dynamics and spine calcium imaging during wake and sleep experiments, we first localized the spines in the xy plane using a maximum intensity projection in time (MIPT). Then, we localized the time point corresponding to the highest intracellular Ca\textsuperscript{2+} level for each spine. We found the Z position containing the three main planes of the spine volume (\(3\mu m\) volume), and performed a Z maximum intensity projection (MIP) time-series of these planes. On the MIP time-series, we delimited a 15 × 15 \(\mu m\) region of interest (ROI) centered on the spine, and generated a new time-series containing only the ROI. Then, we constructed a microglial time-series with the same planes with the same ROI size encapsulating the spine of interest. Finally, standard deviation intensity (STD) projections of the microglial cell images were performed. The maximum intensity and standard deviation projections were used for further analysis of spine activity and microglial dynamics respectively. For most of the microglia-spine analyses, we used 11–22 spines/mouse from five mice. For spine activity during sleep and wake, with and before/after contact, we used 10–18 spines/mouse from five mice. Spines that were not in contact with microglial processes during sleep or wake were excluded from analyses (\(n=16\)). For microglial proximity with dendritic spines, we used 7–15 spines/mouse from 5 mice, including spines that were never contacted by microglial processes. All spines that were very close to microglial cell bodies or primary processes were excluded from the microglia-spine distance analysis.

To quantify calcium activity in spines, we filtered the signal to remove background noise and measured the fluorescence intensity at the center of the spine and calculated the mean (baseline) and the standard deviation of the fluorescence intensity over time. Significant Ca\textsuperscript{2+} events were defined when the fluorescence intensity exceeded 0.3×std above the baseline. This threshold was determined by visual inspection for several spines allowing us a good detection of the Ca\textsuperscript{2+} transients. The Ca\textsuperscript{2+} transient response to the stimulations was expressed as the ratio of the area under the curve (\(\Delta F/F_0\)) prior to and after the stimulus onset over 10 min. Individual calcium transients occurring within 6 s following the stimulation were considered as successful evoked responses. The stimulation success rate has been calculated as the ratio of the number of successful stimulations vs the total number of stimulations. A custom Matlab script that calculates the distance between the center of the spine and the moving front of the closest microglial process was used to measure the distance and contact duration between microglial processes and dendritic spines. Since the size of the spine is variable, the threshold for microglia-spine contact was defined by visual inspection. Physical contacts were defined as a distance lower than 1 pixel between microglial processes and dendritic spines in more than 2–3 consecutive focal planes. The total contact duration was the cumulative time step during which contact was observed.

Spines were categorized into three classes based on the change of activity during the stimulation period: 1) Spines for which the Ca\textsuperscript{2+} activity (\(\Delta F/F_0\)) during the 10 min following the stimulation onset is >1.5 fold the baseline activity was considered as spines responding by an increased activity; 2) Spines displaying a ratio <0.6 were considered as decreased activity spines; 3) Spines exhibiting a ratio in [0.6–1.5] range were considered as stable spines. The thresholds for this classification were established in order to have clear responses to stimulation, homogeneous groups, and blind with respect to microglial contacts and durations of contacts.

Statistics
All statistical analyses were performed using Matlab and the Prism V statistical analysis software (GraphPad, La Jolla, CA). Microglial complexity and motility during the vigilance states were compared by using the non-parametric Wilcoxon test where n-values represent individual animals. Sleep/wake cycles comparison between heterozygous Cx3cr1+/- and homozygous Cx3cr1-/- mice was obtained using a Mann-Whitney test. For EEG spectra comparison between Cx3cr1+/- and Cx3cr1-/- mice, tailed unpaired t-test was performed. For cross-correlation analysis between Cx3cr1+/- and Cx3cr1-/- mice, the peak amplitude P (mean of correlation coefficient at 0, 30, and 60 s) was compared to baseline B (considered from −1000 to −300 s and from 500 to 1000 s as these were considered too far to induce any effects) with Wilcoxon test. For experiments assessing the relationship between microglial dynamics and spine activity, n-values represent individual spines, and we used two-tailed paired t-test or unpaired t-test where appropriate, one-way ANOVA for repeated measures over time, Kolmogorov-Smirnov test for cumulative distributions and Pearson’s correlation test for correlation analyses. Grubbs’ test was applied to identify outliers, and single outliers were removed from the analysis.
values reported are mean ± SEM. A significance p value threshold p < 0.05 was chosen for all analyses.

Reporting summary
Further information on research design is available in the Nature Research Reporting Summary linked to this article.

Data availability
Source data are provided with this paper. Raw image files are stored on servers at Université Claude Bernard Lyon 1 owing to their large size. These raw data can be provided from the corresponding author upon request.

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Author contributions
Conceptualization and experimental design by I.H., K.C., M.R., and O.P. Experiments were conducted by I.H., K.C., and M.R. Data analysis and statistics were performed by I.H., K.C., M.R., and J.C.C. Codes were written by J.-C.C. The manuscript was written by I.H., K.C., M.R., and O.P. with contributions from J.-C.C. and J.H.

Competing interests
The authors declare no competing interests.

Additional information

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