Collective charge fluctuations in single-electron processes on nanonetworks

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Abstract. Using numerical modeling we study the emergence of structure and structure-related non-linear conduction properties in self-assembled nanoparticle films. In particular, we show how different nanoparticle networks emerge within assembly processes with molecular bio-recognition binding. We then simulate the charge transport under voltage bias via single-electron tunnelings through the junctions between nanoparticles on such networks. We show how the regular nanoparticle array and topologically inhomogeneous nanonetworks affect the charge transport. We find long-range correlations in the time series of charge fluctuation at individual nanoparticles and of flow along the junctions within the network. These correlations explain the occurrence of a large non-linearity in the simulated and experimentally measured current–voltage characteristics and non-Gaussian fluctuations of the current at the electrode.

Keywords: transport properties (theory), network dynamics, nonlinear dynamics
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1. Introduction

Functional soft materials composed of many nanoparticles often appear in complex structure both as two-dimensional films [1, 2] and as three-dimensional super-crystal structures [3]–[5]. These structures emerge in various processes of self-assembly, most of which utilize liquid degrees of freedom and non-equilibrium methods [6, 7]. The gold nanoparticles are often used due to the property that their surfaces can be functionalized in an appropriate manner. The functionalization of the nanoparticle surfaces has effects on their interactions [8]. In the case of nanoparticle films on substrate assembled by liquid evaporation [9], thiol-passivated nanoparticles were used, where the attached chains determine the minimum distance between two neighboring nanoparticles. Another way to induce desired interaction between two nanoparticles was designed recently with attaching pieces of biologically compatible strands of DNA molecules to different nanoparticles [3]. The DNA-mediated interaction then utilizes the biological recognition and binding energy of the compatible DNA base pairs. Depending on a number of other factors, which we will also discuss later, this programmable self-assembly may lead to random as well as regular super-crystal structures, as shown in recent experiments in [3]–[5]. Somewhat similar (but in a different potential range) is the bio-recognition assembly which utilizes biologically compatible protein molecules, for instance the antigen–antibody recognition [10], which can be used in biosensors.

The nanoparticle assemblies exhibit a wide range of physical properties which are not found in the bulk materials and at the level of a single nanoparticle [8]. Moreover, the emergent physical properties of the nanoparticle assemblies can often be related to their spatial structure [4, 5, 7, 11]. For instance, new optical and magnetic properties have been found in super-lattices made of nanocrystal [11]. On specific functionalization of their surfaces, gold nanoparticles develop directionally dependent exchange interaction [12].

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Assuming that such nanoparticles can be arranged on nodes of a sparse scale-free graph, numerical simulations predict new features of the magnetic response of such a structure [13,14], compared to the classical memory materials [15]. Similarly, the films of gold nanoparticles under voltage bias conduct current via \textit{single-electron tunneling} processes [16] due to their small capacitances and the Coulomb blockade effects [17]. In comparison to classical conduction, single-electron conduction processes have numerous advantages, e.g., the absence of dissipation due to heating, and the non-linear current–voltage characteristics, which are important in nanoelectronics. Experimentally, a large non-linearity of the current–voltage curve was found for self-assembled nanoparticle films on substrates, which appears to be fairly well correlated with the film structure [1,18,19].

The random structure of nanoparticle films on substrates can be adequately modeled by planar graphs (nanonetworks) [18,21]. For the charge transport via single-electron processes, which we study here, the topological elements of these nanonetworks are suitably selected as follows: the \textit{nodes} represent nanoparticles, whereas \textit{edges} (links) are the tunneling junctions between two nanoparticles. For the junction (link) to occur between two nanoparticles, the distance between them must be smaller than the \textit{tunneling radius} of the electrons for that kind of nanoparticle [17]. The charge transport through the film under applied voltage can be described within the model of the capacitively coupled nanoparticles on substrates [22]. In our previous work [23] we generalized the model of capacitively coupled nanoparticle assemblies for an arbitrary topology of the nanonetworks [18,23] and implemented a numerical model of single-electron tunnelings driven by the external voltage through such networks. Theoretical background and the details of the numerical implementation are reviewed in [23]. The simulation results revealed the topology-induced non-linearity in the \( I(V) \) curve, in a good agreement with the experiments [18].

In the present work we study the collective dynamic behavior which makes the physical basis for the observed \( I(V) \) non-linearity, in particular, the long-range correlations in charge fluctuations monitored at each nanoparticle and inhomogeneous charge flow along the conducting paths through the sample and at the electrode. We determine the probability distributions of various quantities related to the conduction process and demonstrate how the topological and charge disorder affect the quantitative statistical properties and the \( I(V) \) dependences.

The organization of the paper is as follows. In section 2 we present the model of the particle self-assembly with bio-recognition bonding and show some of the typical emergent structures. In section 3 we summarize the theoretical background of the conduction with single-electron processes and its numerical implementation for an arbitrary network topology. The visualization of the conduction paths through two network types, the regular and inhomogeneous nanoparticle aggregates, as well as the statistical properties of the topological and charge flow, are shown in section 4. In section 5 we analyze the simulated time series of charge and current fluctuations and the related \( I(V) \) curves. Section 6 gives a short summary of the results.

2. Nanoparticle networks emerging in self-assembly with bio-recognition

Different assembly processes make use of the liquid phase, that provides the nanoparticle diffusion and affects the interaction. The assembly with fast evaporation of the liquid [1,9]
induces additional constraints to the particle motion and interaction. The interaction itself between pairs of the nanoparticles moving in a liquid is taking place at short distances and depends on the type of functionalization of their surfaces [24], as mentioned above. In the case of bio-recognition binding [25], which we will discuss shortly, the attached DNA induces differences between two kinds of nanoparticles, i.e., type A and type B nanoparticles, each of which carry the biologically compatible strand of the same DNA molecule. Thus, the interaction between A and B types is attractive within some bonding distance $d_b$. The bonding distance depends on the lengths of the attached molecules and on the number of their compatible base pairs [4, 25]. Therefore, it exceeds the sum of the particle radii, $d_b > R_A + R_B$. The effective interaction between A and B particles can be then modeled by the Lennard-Jones potential [24]

$$V_{A-B}(r) = 4\epsilon \left( \frac{\sigma_{12}^{12}}{(r - R_A - R_B)^{12}} - \frac{\sigma_6^6}{(r - R_A - R_B)^6} \right),$$

(1)

where $r$ is the actual distance between particles and the potential minimum corresponds to the optimal bonding distance. In the present case, the parameters $\sigma$ and $\epsilon$ depend, roughly speaking, on the lengths of the attached DNA chains and the strength of binding (number of the compatible base pairs) [7]. In contrast, the particles which carry biologically incompatible DNA strands have no attractive interaction of this type. The repulsive part alone of the potential in equation (1) can describe the interaction of the equal-type particles A–A and B–B, occurring at short distances. We assume that a large number of ligands are added symmetrically on each nanoparticle, which pertains to the spherical symmetry of the potential. Note also that, due to the geometrical constraints and the repulsive interactions between similar particles, the maximum coordination number is always finite and determined by the relative size of the particles.

The diffusion of such nanoparticles can be simulated via the Langevin equation with the random force originating from the integrated liquid degrees of freedom and the thermal fluctuations [26]. Apart form the molecular difference between attached DNA strands, generally, the particle radii $R_A \neq R_B$ can be different and consequently two different diffusion coefficients $D_i$ enter the equation

$$\nu_i \dot{r}_i = -\nabla_{r_i} \sum_j V_{i-j}(|r_i - r_j|) + F_{i,T},$$

(2)

with $\langle F_{i,T}(t) \rangle = 0$, $\langle F_{i,T}F_{j,T}(t') \rangle = 6k_BT\nu_i \delta_{i,j} \delta_{t,t'}$, and $D_i = k_BT/\nu_i$, $i$ referring to either the A or the B particle type. A complete description of the model and the discussion of the role of different parameters in the self-assembly processes will be given elsewhere [26]. Here we restrict our discussion to the situation which is interesting for the assembly of the conducting nanoparticle films. Therefore, we consider particles of equal size $R_A = R_B$, and vary the relative concentration $c_A : c_B$ of particles A and B carrying different strands of the molecule. In this way various structures can be assembled, both regular and irregular, which in turn appear to have different physical properties (as discussed below). For fixed parameters of the potential, temperature $T$ and the diffusion coefficients $D_i$, we start with a given number of particles $N_A$ and $N_B$ at random positions in a box of size $L \times L$. Using the fourth-order Runge–Kutta method we solve the differential equation (2) for the trajectories of both particle types. At each time step $k \times \Delta t$ the positions of all particles are updated in parallel, where small $\Delta t$ is used to maintain the smooth potential changes and
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Figure 1. Two examples of the emergent nanoparticle films obtained via bio-recognition binding between A (red) and B (yellow) particles for equal coverages and different relative concentrations \( c_A/c_B \) as follows: 25%:75% (left) and 50%:50% (right).

reflective boundaries are assumed. The random Langevin force \( F_{i,T} \) in equation (2) is taken from the normal distribution at each time step. The relevant control parameter *coverage* is defined as the fraction of the surface covered by the particles, which depends on their concentrations and size (including their bonding radius). In these simulations we keep the temperature fixed to a low value \( k_B T/\epsilon = 0.1 \), which ensures enough diffusive motion. At the same time, the bonds formed between pairs may break with the Boltzmann weight, which rarely occurs at this temperature. Thus this non-equilibrium assembly leads to generally different structure for different initial conditions. However, these structures are statistically similar for the same set of control parameters, and correspond to a different local minimum of the free energy of the whole system. A lower minimum is found in the case of regular structures, i.e., for equal concentrations \( c_A = c_B \) of bonding particles. The assembly processes and the emergent structures for the full parameter range will be discussed elsewhere [26].

In figure 1 we show two representative structures which emerge in the process when temperature is kept low compared to the parameter \( \epsilon \), and the total coverage of the surface by particles is fixed, but the relative concentrations of A and B particles varied. Generally, for low enough temperatures and equal concentrations the system has a tendency towards a *regular* ordered structure with few defects (figure 1, right), whereas, when the concentrations are not in balance, another type of structure with local order and large voids may appear, as shown in figure 1, left. It should be stressed that, for a fixed set of parameters, many such structures may appear depending on the initial conditions. Each of them corresponds to a local free energy minimum, and appears to be quite stable for the low temperatures [26]. In the following we will discuss in detail the conduction properties of a regular nanoparticle structure and of a highly irregular nanoparticle structure on the substrate. In practice, the regular (triangular) nanoparticle arrays [19] and irregular nanoparticle films [2] are assembled using entirely

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different approaches. Our results shown above demonstrate that such diverse structures may appear in the same self-assembly process with bio-recognition when a single parameter (the relative concentration of differently functionalized nanoparticles) is suitably varied.

3. Single-electron tunnelings in nanoparticle films

The capacitively coupled nanoparticle assembly on a substrate under an applied voltage conducts current with a cascade process of single-electron tunnelings, which is enabled by the Coulomb blockade at junctions between the adjacent nanoparticles [17, 22]. Following a single-electron tunneling through the junction between two particles $a \rightarrow b$, the charging energy of the nanoparticle increases inversely proportionally to its capacitance. This increases the barrier for further tunnelings along that junction, and consequently, no tunnelings occur until the voltage is increased enough to overcome the barrier.

The theoretical background of the tunnelings within the nanoparticle arrays has been developed in [20, 22]. Recently we have generalized the formulation for the case of nanonetworks with the tunneling junctions representing the network edges [23]. It should be stressed that the links in the nanonetwork suitable for the tunneling processes might differ from those of the bio-recognition binding, shown in figure 1. Specifically, for the tunneling processes, of importance are positions of the nanoparticles on the substrate and their mutual distances compared to the tunneling radius $r_t$. The chemical bonds, which are shown in figure 1, are to be understood as fixing the nanoparticle positions. Then the tunneling junction network may have links which coincide with the chemical bonds only when the bonding distance $d_b \sim r_t$; otherwise, the tunneling junction network is different. Generally, the nanonetwork edge representing the tunneling junction occurs between any two nanoparticles which are separated at distances $r \leq r_t$. In addition, the difference between A and B particle types, which was important for the assembly, plays no role in the conduction (assuming the particles of the same size and chemical composition). In this way, a nanonetwork of tunneling junctions can be constructed whenever the positions of the nanoparticles on the substrate are known [27]. In our numerical models the tunneling radius is a free parameter. Varying the tunneling radius, e.g., by changing the chemical composition and size of the nanoparticles, slightly different nanonetworks of junctions can be constructed. For the numerical implementation of the tunneling process the nanonetwork of tunneling junctions is fixed by the adjacency matrix with the elements $A_{ij} = 1$, when the tunneling between the nanoparticles $i$ and $j$ can occur, and $A_{ij} = 0$, when the junction is absent, e.g., due to the large distance $d_{ij} > r_t$ between them. In the following we consider two such nanonetworks: a regular triangular array, representing the realistic structure of [19], and an inhomogeneous network obtained by a highly non-equilibrium evaporation process, as described in [18].

3.1. Electrostatic energy of a nanoparticle network

Following the classical work [22] the electrostatic energy for a capacitively coupled nanoparticle array consisting of $N$ nanoparticles and of a general topology given by the adjacency matrix $\{A_{ij}\}$ can be described as follows [23]. The capacitances are related

\[ E \propto \sum_{i,j} A_{ij} C_{ij} \

\text{where } C_{ij} \text{ is the capacitance between nanoparticles } i \text{ and } j. \]
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to the structure of the underlying nanonetwork by $C_{ij} \equiv CA_{ij}$. The charge $Q_i$ on the $i$th nanoparticle can be expressed as

$$Q_i = \sum_j C_{ij} (\Phi_i - \Phi_j) + \sum_\mu C_{i,\mu} (\Phi_i - \Phi_\mu),$$

where $\Phi_i$ is the potential of the $i$th nanoparticle in the assembly. The index $\mu \in \{+, -, g\}$ is attributed to the electrodes (including the gate) and thus $\Phi_\mu$ is the potential at the $\mu$th electrode and similarly $Q_\mu$ is the charge and $C_{i,\mu}$ the capacitance of the $\mu$th electrode and $i$th nanoparticle. The system of equations (3) for $i = 1, 2, \ldots, N$ can be written in the matrix form $Q = M\Phi - C_\mu \Phi_\mu$ and formally solved for $\Phi$ as

$$\Phi = M^{-1}Q + M^{-1}C_\mu \Phi_\mu,$$

where now $M$ is the capacitance matrix of the whole system (nanoparticles plus electrodes) with the elements given by

$$M_{ij} = \delta_{i,j} \left( \sum_k C_{ik} + \sum_\mu C_{i,\mu} \right) - C_{ij}.\quad (5)$$

Using these definitions, the electrostatic energy of the whole system can be written as

$$E = \frac{1}{2}Q^\dagger M^{-1}Q + Q \cdot V_{ext} + Q_\mu \Phi_\mu, \quad V_{ext} = M^{-1}C_\mu \Phi_\mu,$$

where $\mu \in \{+, -, g\}$ stands for the electrodes and gate, $V_{ext}$ is the external voltage, $C_{i,\mu}$, $Q_\mu$, $\Phi_\mu$ are defined above.

3.2. Numerical implementation and visualization of charge transport

The system is driven by increasing the external voltage at one, say the left, electrode. The voltage on the gate is kept fixed. Due to the voltage bias, the electrons first tunnel from the left electrode to the neighboring nanoparticles and then forward along the available junctions between the nanoparticles. Due to the overall voltage profile the tunneling is predominantly to the right, towards the zero-voltage electrode as $+V \rightarrow a \rightarrow b \rightarrow \cdots \rightarrow 0$.

Following the tunneling of a single electron from particle $a \rightarrow b$, causing the change in the particle charges as $Q_i^\prime = Q_i + \delta_{ib} - \delta_{ia}$, the energy change $\Delta E(a \rightarrow b)$ occurs in the whole array, due the long-range interactions. The energy change is computed using the expression in equation (6) as follows:

$$\Delta E(a \rightarrow b) = V_b - V_a + \frac{1}{2}(M_{aa}^{-1} + M_{bb}^{-1} - M_{ab}^{-1} - M_{ba}^{-1}) + V_{ext}^b - V_{ext}^a,\quad (7)$$

and similarly $\delta E(a \leftrightarrow \pm) = \pm V_a + \frac{1}{2}M_{aa}^{-1}$ originating from the tunneling between the electrode and the nanoparticle. Here we have defined the following quantity:

$$V_c \equiv \sum_i Q_i M_{ic}^{-1},$$

which is also suitable for the numerical implementation. Namely, the updated value of the variable $V_c$ at node $c$ following the tunneling $a \rightarrow b$ can be computed recursively as follows:

$$V_c^\prime = V_c + M_{bc}^{-1} - M_{ac}^{-1}, \quad a \rightarrow \pm : \quad V_c^\prime = V_c \pm M_{ac}^{-1}. \quad (9)$$

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The simulation takes the following steps: for the fixed voltage $V$ the whole network is updated for tunnelings. For each junction the attempted tunneling from $i \rightarrow j$ induces the global energy change $\Delta E_{i \rightarrow j}$, which is computed using the above formulae. Then the tunneling rate for the $i \rightarrow j$ event at given voltage $V$ is computed according to \cite{23}
\begin{equation}
\Gamma_{i \rightarrow j}(V) = \frac{1}{eR_{i \rightarrow j}} \frac{\Delta E_{i \rightarrow j}}{1 - e^{-\Delta E_{i \rightarrow j}/k_B T}},
\end{equation}
where $e$ stands for the electron charge, $T$ is the temperature and $R_{i \rightarrow j}$ is the quantum resistance of the junction. The quantum resistance (or conductance) can be computed for small nanoparticles. e.g., using density functional theory \cite{28}. For instance, for the metallic nanoparticles one can obtain within the transfer Hamiltonian that
\begin{equation}
R_t = \frac{\hbar}{2\pi e^2 |T| D_0 D_r 0},
\end{equation}
where $T_0$ and $D_0$ are the transmission coefficient and the density of states at each nanoparticle \cite{17}. We assume that the quantum resistance $R_{i \rightarrow j} \equiv R_t$ for all junctions. Note that in the approach described above, $R_t$ appears as a parameter which sets the characteristic timescale of the process via $\tau \sim 1/R_t C_g$ (see later). In our continuous time implementation, out of all attempted tunnelings only those whose tunneling times $t_{i \rightarrow j}$ taken from the probability distribution $p(t_{i \rightarrow j}) = p_0 \exp(-\Gamma_{i \rightarrow j} t)$ appear to be in small time window $\delta t$ are processed. Then the network is updated again (for more details see \cite{23}). Here we use the limit $C/C_g \ll 1$ and $V_g = 0$.

When the external voltage is increased, more electrons tunnel into the nanoparticle array and consequently the local ratio between the charge and voltage is changed, providing the conditions for more forward tunnelings. The moving front of charges on the slab of regular triangular arrays of nanoparticles is shown in figure 2 for a set of different voltages. The color intensity indicates the number of electrons at the nanoparticle. When the voltage is large enough $V \sim V_T$, the moving front reaches the zero-voltage electrode and the current through the sample can be detected for the first time. For the voltages $V > V_T$ the current through the sample is non-zero for all times. The average current through the junction $i \rightarrow j$ is defined as the net number of electrons per time unit:
\begin{equation}
I_{i \rightarrow j}(V) = e \left( \Gamma_{i \rightarrow j}(V) - \Gamma_{j \rightarrow i}(V) \right).
\end{equation}

In the numerical experiment we can measure the current through each junction within the film and at the electrode. In the laboratory experiments the current is measured

\textbf{Figure 2.} Visualization of the charge profile before the voltage threshold is reached.
Figure 3. Visualization of the conduction paths through the regular triangular array with charge disorder at nodes (left) and through the topologically inhomogeneous network without charge disorder (right). For a fixed voltage \( V > V_T \) the cumulative charge flow along each link is recorded and represented by the color intensity.

only at the electrode. The current increases with voltage. However, the current–voltage dependence appears to be non-linear for a range of voltages above the threshold \( V > V_T \):

\[
I(V) = B \left( \frac{V - V_T}{V_T} \right)^\zeta; \quad \zeta > 1.
\] (12)

The exponent \( \zeta \) was found to vary from 2 to 4 with the structure of the nanoparticle arrays; in particular \( \zeta = 2.25 \) was measured in the case of regular triangular array of gold nanoparticles [20], whereas \( \zeta = 3.9 \) and larger was found in highly inhomogeneous films obtained by the evaporation methods [18]. As mentioned in the introduction, one of the purposes of the present work is to study the charge and current fluctuations inside the sample in order to reveal the correlations in the process which contribute the observed non-linearity in the current–voltage curves. The other aim is to demonstrate the role of random charge disorder in the transport process. The charge disorder represents fractional charges which are locally present in the real samples, for instance, due to differences in the contacts of some nanoparticles with the substrate, and affect the charge–voltage relation at these nanoparticles. In the simulations we consider the regular triangular array of nanoparticles with quenched charge disorder \( 0 < q_i < 1 \) at the \( i \)th nanoparticle taken from the uniform random distribution. The calculations are systematically compared with the case for a nanoparticle film without charge disorder but with large topological inhomogeneity of the structure (figure 3).

4. Topological and charge flow: conducting paths

For voltages over the threshold \( V_T \) the conducting paths through the sample are established. By recording the current through all junctions in the network we can

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visualize the charge flow along these conducting paths, as shown in figure 3. Darker color corresponds to larger number of electrons transported along the link. Figure 3 also demonstrates the role of topological inhomogeneity, i.e., in the case of the nanonetwork in the right panel, as opposed to the regular nanoparticle array. In the inhomogeneous nanonetwork, the areas without nanoparticles place a restriction on the charge transport; thus the conducting paths merge into a smaller number of paths in the bottleneck regions. Draining the electrons along such paths thus affects a large region behind. This also indicates that certain nodes on the paths play more important roles in the charge flow than the others. The quantitative measure of the node importance is the topological betweenness-centrality $B$, which is defined as the number of shortest paths between all pairs of nodes on the graph that go through that node. In the case of the inhomogeneous film network in figure 3 (right), the topological betweenness-centrality is given by a broad distribution with a power-law tail, shown in figure 4 (left). In the regular nanoarray, in contrast, the topological betweenness-centralities of all nodes are similar (not shown), which induces a less intricate pattern of conducting paths. In figure 3 (left) we show the conducting paths in the case of a triangular array in the presence of charge disorder. As already mentioned above, the presence of a random fractional charge at nanoparticle may destroy the local balance between the voltage and charge, leading to blocking of certain conducting paths through that nanoparticle and consequently reduced charge transport through that particle. Such areas with reduced charge flow appear as bright spots in figure 3 (left). The dynamical betweenness-centrality or charge flow $F$ of a junction on the network is defined as a number of electrons tunneling through that junction within a large time window. The distributions $P(F)$ for both networks are shown in figure 4 (right). Again the differences between two topologies play a role. In the inhomogeneous network NNET1, the distribution of the charge flow along the links on this network resembles the distribution of topological betweenness (one should stress that the shortest paths between the electrodes play this role in the conduction). The simulation results can be approximately fitted with the $q$-exponential form \cite{29} $P(F) \sim [1 - (1 - q)(F/F_0)]^{1/(1-q)}$.

\textbf{Figure 4.} Distribution of the topological flow $\mathcal{B}$ in the inhomogeneous nanonetwork NNET1 (left) and distributions of charge flow $F$ along the links in NNET1 and in the triangular nanoparticle array with charge disorder (right).
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Figure 5. Left: current plotted against reduced voltage for the topologically inhomogeneous nanonetwork NNET1 (bottom curve) and for several regular structures: one-dimensional, hexagonal and triangular arrays with charge disorder, and triangular arrays without charge disorder. Right: distributions of the increments of current fluctuations $P(\Delta I)$ against $\Delta I$ for the triangular array with and without charge disorder and for the topologically disordered NNET1. Fits: $q$-Gaussian according to equation (13).

with $q = 1.05$. In the case of the triangular array with charge disorder, the distribution indicates that certain links in the network carry less charge during the conduction process. The curve $P(F) \sim (1/F) \exp[\ln(F/F_0)]$ approximates the numerical results near the peak of the distribution.

5. Non-Gaussian current and charge fluctuations

In our simulations the current recorded at the right electrode for the applied voltages above the threshold $V > V_T$ can be compared with the experimental measurements on the nanoparticle films [18, 20]. The threshold $V_T$ depends on the network size (distance between the electrodes) and its structure.

5.1. Current–voltage curves

In figure 5 (left) the current at the electrode is shown against reduced voltage $(V - V_T)/V_T$ obtained in the simulations on different nanonetworks. It is clear that for a wide range of voltages the dependences $I(V)$ are non-linear with $\zeta > 1$ according to equation (12) for all two-dimensional nanonetworks. We have also shown the simulations for the one-dimensional array of nanoparticles for comparison. For the electron tunnelings through the one-dimensional chain of nanoparticles the exponent remains $\zeta = 1$ (top curve in figure 5). However, in the two-dimensional samples many conducting paths may open between the electrodes. Flow along these paths is a dynamical process with long-range correlations. The contributions of flow along different paths builds up the cumulative
current which is measured at the electrode. Therefore, different geometries have different patterns of the conducting paths (as also shown in figure 3), leading to different non-linear effects in the current–voltage dependences. Generally, the regular structures have smaller exponent; for instance, we find $\zeta \approx 2.25$ for the triangular array with charge disorder, in very good agreement with the experiment [20]. A slightly larger exponent is found for a hexagonal nanonetwork without charge $\zeta \approx 2.8$, whereas for the inhomogeneous nanonetwork NNET1 we have $\zeta \approx 3.9$, within the numerical error. The exponents in this range are found for other inhomogeneous nanoparticle films both in the simulations and in the experiment [18].

It is interesting that such cooperative effects of different paths occur in a limited range of voltages $V > V_T$, approximately one order of magnitude on the reduced voltage scale (see figure 5). In this range of voltages, the draining of the electrons along a conducting path is intermittent and induces an avalanche of flows in the connected area of the network. However, when the voltage is large enough, a permanent flow along each paths sets in, making them chain-like, and consequently the $I(V)$ curve exhibits a crossover towards the linear dependence.

5.2. Time series analysis

In complex dynamical systems, time series of fluctuating variables contain valuable information about the correlations in the dynamical process [30]. In the case of the single-electron transport through the nanoparticle films, we consider temporal fluctuations of the current, which is measured at the electrode, and also the fluctuations of the charges (number of tunnelings) between all nanoparticles inside the sample.

For the current, which is measured at the electrode, we consider the time series of the current $\{I(t)\}$, given in figure 6, and the increments of the current $\{\Delta I(t)\}$, which is a measure of the acceleration in the electron transport along the conducting paths. Each point is averaged over time window $t_{WIN} = 100$ time steps (updates of the whole network).

In figure 5 (right) we have shown the distributions of the increments $P(\Delta I)$ obtained for

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Figure 7. Time series representing the number of tunnelings and their corresponding power spectra in (left) the triangular array with charge disorder and (right) the topologically inhomogeneous NNET1 (data from [23]).

A fixed voltage above the threshold, for the triangular array with charge disorder and for the topologically disordered nanoparticle array NNET1. The distributions are fitted with the $q$-Gaussian [29, 31]

$$P(\Delta I) = B \left( 1 - (1 - q) \left( \frac{\Delta I}{D_0} \right)^2 \right)^{1/1-q};$$

with different $q$ values for different nanoparticle arrays: $q = 1.14$ for the geometrically regular triangular array with charge disorder, while $q = 1.85$ for the topologically inhomogeneous NNET1. Similarly, the analysis of the time series of the current itself, \( \{I(t)\} \), exhibits different correlations in these two geometries. In figure 6 the power spectra of the time series are shown. The spectrum of the topologically inhomogeneous NNET1 shows the long-range correlations as $S(\nu) \sim 1/\nu$ at high frequencies, whereas the spectrum flattens at high frequencies in the case of the triangular charge-disordered array. At low frequencies, however, weak correlations are observed in both networks.

The correlations in the current fluctuations at the electrode, i.e., at the last layer of the nanoparticles connected to the electrode, are caused by the tunneling processes deeper in the sample. The time series of the number of tunnelings \( \{N_T(t)\} \) at all nanoparticles in the whole network and their power spectra are shown in figure 7. The power spectrum of the number of tunnelings exhibits long-range correlations for high frequencies, according to

$$S(\nu) \sim \nu^{-\phi}.$$  

The exponent $\phi = 1$ (within numerical error bars) for the topologically disordered nanonetwork NNET1 suggesting strong cooperation between the conducting paths, whereas the correlations are much weaker in the triangular array.

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6. Conclusions

In our numerical study of the conducting nanoparticle films on substrates, we pointed out several steps that play an important role in designing the conduction properties of the films. Specifically, we study in quantitative detail the emergent properties of such nanoparticle assemblies along the line from the self-assembly processes, the topology of structures, and conduction through such structures.

- **Self-assembly** processes are leading to different kinds of structures of the film. We have shown that both regular and highly inhomogeneous nanoparticle films, which are typically fabricated by entirely different techniques [9, 19], can be assembled within the same process with the bio-recognition binding and varying a single control parameter.

- **Conducting paths** through the film have been identified and their topological centrality and the dynamical flow computed for $V \geq V_T$. Coalescence of flow along different paths contributes to the non-linear $I(V)$ dependences for a range of voltages above the transition $V_T$. In our simulations, the non-linearity exponent $\zeta$ depends strongly on the structure, in agreement with measured $I$–$V$ curves of different nanoparticle films [1], [18]–[20]. Blocking the paths due to the charge disorder leads to reduced exponent $\zeta$ compared to same geometry without disorder.

- **Collective dynamical effects** in the tunneling processes deep inside the sample lead to non-Gaussian current fluctuations at the electrode. We have determined various statistical measures of these collective effects. In particular, we find long-range correlations in charge fluctuations at all nanoparticles, broad distribution of flow on junctions through the nanonetwork, and non-Gaussian distribution of the current increments on the electrode. A non-Gaussian distribution has been found in the experiments with nanowires [32]. Our numerical results suggest that $q$-Gaussian distributions with different parameters could be measured in the nanoparticle films. Different values of $q$ for $P(F)$ and $P(\Delta I)$ on the same network merely represent different power-law tails of the distributions of these two stochastic variables. The expressions like equation (13) also suggest deviation from the power law below a characteristic scale $D_0$ in both distributions. The occurrence of the $q$-Gaussian for a larger class of complex dynamical systems with long-range interactions has been discussed recently [33].

Furthermore, we demonstrate how different types of disorder affect the conduction in our comparative study of the regular nanoparticle array in the presence of local charge disorder, on one hand, and the topologically inhomogeneous nanonetwork without charge disorder, on the other. We hope that our detailed numerical study of the processes leading to different structures and the structure-dependent function of the nanoparticle assemblies sheds new light on the problem of engineering of functional materials with desired characteristics.

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