A Model-Free Approach to Low-Dose Extrapolation
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Introduction
The goal of cancer risk assessment is to predict the risk of tumor occurrence in people exposed to carcinogenic agents present in the environment. Such estimates of risk are useful in assessing the potential health impact of such exposures and in evaluating risk management strategies for exposure mitigation. In practice, cancer risk assessment is a complex process for a complex disease. There are many different forms of cancer, many with different disease etiologies. There exists uncertainty regarding the mechanisms of initiation, promotion, and progression of neoplastic changes; the pharmacokinetic distribution of reactive carcinogenic metabolites within exposed individuals; and the pharmacodynamic effects of the proximate carcinogen in target tissues.

The most relevant data for prediction of cancer risk are derived from human populations subjected to well-characterized conditions of exposure resulting in an elevated level of risk. Epidemiological data have been of great value in identifying a number of agents capable of causing cancer in humans, particularly through observations on certain occupational groups or individuals exposed to moderately high levels of the agent of interest. To estimate the potential risks associated with lower environmental exposures, downward extrapolation of these results may be required.

In many cases, epidemiological data on a suspect carcinogen may be nonexistent or inadequate for purposes of quantitative risk assessment. This can occur due to a lack of accurate information on exposure levels or the presence of confounding risk factors. In this event, prediction of human cancer risks may be attempted using laboratory studies of carcinogenicity, on the basis that animal carcinogens are presumptive human carcinogens (I) and that some degree of correlation in carcinogenic potency exists between animals and humans (2). Because of the need to elicit potential toxic effects using a limited number of experimental subjects, the doses used in laboratory studies are generally much higher than human exposure levels. Consequently, the need to extrapolate from high to low doses also arises with toxicological data.

Past approaches to the low-dose extrapolation problem have relied on an assumed mathematical function relating cancer risk to exposure. There are many different candidates for such a dose-response model, some with stronger biological bases than others (3). Tolerance distribution models such as the probit and logit have generally evolved in the study of noncarcinogenic endpoints to describe dose-response relationships in the observable response range. Mechanistic models describe carcinogenesis as a stochastic multistage process, in which neoplastic conversion of stem cells proceeds through a series of well-defined stages involving both genetic damage and changes in cell kinetics. Unfortunately, with the limited information provided by epidemiological and toxicological studies, it is possible to postulate different models that fit the data equally well, but which provide point estimates of risk at low doses that differ by several orders of magnitude (4).

The purpose of this paper is to provide a procedure for low-dose risk estimation that does not depend upon the selection of a specific dose-response model. Our goal is to obtain the best possible upper confidence limit on low-dose risk using only data on tumor occurrence rates from epidemiological or toxicological studies. The only assumption made is that the underlying dose-response curve is linear or sublinear at low doses. Estimates of low-dose risk based on the model-free procedure proposed in this paper are compared with corresponding estimates based on the linearized multistage model using a large number of data sets previously reported in the literature.

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Carcinogenic Risk Assessment

Multistage Model

The multistage model is currently the most widely used model for cancer risk estimation. As formulated by Armitage and Doll (5), the probability \( P(d) \) of a tumor occurring following exposure to a fixed dose \( d \) up to time \( t \) is given by

\[
P(d) = 1 - \exp \left[ -ct^k \sum_{i=0}^{n} (a + b_i d) \right]
\]

(1)

where \( i = 1, \ldots, k \) indexes the distinct stages of a \( k \)-stage process. Here, \( a + b_i d \) represents the rate at which transitions to stage \( i \) occur, with \( a > 0 \) denoting the spontaneous transition rate and \( b_i d (b_i \geq 0) \) representing the effects of dose \( d \). The constant \( c \) is proportional to the number of individual cells at risk in the target tissue.) This model predicts that the age-specific cancer incidence rates will be proportional to age raised to the power \( (k-1) \) and provides a good description of human cancer incidence curves with \( 2 \leq k \leq 6 \).

For applications, Crump et al. (6) proposed the modified multistage model

\[
P(d) = 1 - \exp \left[ -ct^k \sum_{i=0}^{n} (q_i d) \right]
\]

(2)

where the \( q_i \geq 0 \). Although the class of polynomials with non-negative coefficients included in the exponent in Eq. (2) is broader than the corresponding class in Eq. (1), this formulation is easier to apply in terms of parameter estimation. For small \( d \), we have

\[
P(d) - P(0) = q_i d \frac{1 - P(0)}{1 - P(d)}
\]

(3)

Thus, when the background \( P(0) \) is small, \( q_i \) represents the slope of the dose-response curve in the low-dose region. Although the original model [Eq. (1)] is linear at low doses, the extension in Eq. (2) allows for the case \( q_i = 0 \). In practice, an upper confidence limit \( q_i^{(0)} \) is used, which will be strictly positive (7). This upper bound has come to be known as \( q^2 \) and provides a measure of carcinogenic potency based on the linearized multistage (LMS) model.

Point Estimates Versus Confidence Limits

The use of a 95% upper confidence limit on \( q_i \) rather than its maximum likelihood estimate has been the subject of some discussion. Proponents of best estimates argue that the use of upper confidence limits leads to unwarranted conservatism in risk estimation (8). When decision-making allows for balancing risks against benefits, it has also been argued that best estimates of benefit should be compared to best estimates of risk. Upper bounds on risk based on the linearized multistage model have also been criticized in that they are highly insensitive to the data on which they are based (9).

For various reasons, the U.S. Environmental Protection Agency (10) has taken the position that, in general, best estimates of risk cannot be reliably computed at this time. In the absence of a suitable best estimate of risk, the Agency advocates the use of linearized upper bounds. This position is based in part on the fact that the best estimate of \( q_i \) may be 0, in conflict with the strict linearity implied by Eq. (1). Even when positive, the maximum likelihood estimator of \( q_i \) can be relatively unstable, with minor perturbations to the data resulting in marked changes in its estimated value (11).

Biologically Based Cancer Models

The Armitage-Doll model has been subject to criticisms that it does not provide a complete description of the process of carcinogenesis. Specifically, the \( k \)-stages envisaged in the model are largely phenomenological and do not necessarily represent well-defined biological changes. In particular, when the number of stages required to fit the data is large, it is difficult to interpret these stages as specific mutational events. The model also fails to provide for the development of target tissues with age and for the dynamics of cells involved in neoplastic conversion.

Moolgavkar (12) and his co-workers (13,14) have developed a two-stage biologically based model of carcinogenesis that explicitly provides for tissue growth and cell kinetics. This model assumes that two mutations, each occurring during cell division, are required for a stem cell to be transformed into a malignant cancer cell. Initiated cells that have sustained the first mutation may be promoted through nongenotoxic mechanisms that increase the net birth rate of initiated cells. Thorslund and Charnley (15) have applied a form of this model in the estimation of cancer risks associated with exposure to chlordane and dioxin. However, the estimability of the unknown model parameters requires further study (16).

Range-of-Risk Estimates

Since precise mechanisms of carcinogenic action are generally unknown, it follows that no model, no matter how elaborate, can claim to be correct. This uncertainty has prompted proposals for the use of a range-of-risk estimates based on different plausible models. Calculation of a range-of-point estimates serves little purpose and does not contribute to a real understanding of the uncertainty in the extrapolation process. Since point estimates depend on the form of the model selected, the number of point estimates is limited only by the number of models entertained.

In our view, a more realistic approach to expressing uncertainty is to recognize that the risk could be as high as or higher than one-hit extrapolation or as low as 0. The risk will be 0 when a threshold exists below which neoplastic conversion does not occur. Pyne et al. (17) have suggested that a threshold may exist for thyroid tumor induction, although the evidence in this regard is not conclusive.

Is Linear Extrapolation Conservative?

Linear extrapolation often is criticized as being too conservative. Schell and Leysieffer (18) show that the one-hit model, which is linear at low to moderate doses, provides an upper
bound on risk for any dose-response model satisfying an increasing failure rate condition with dose. (This condition holds for commonly encountered dose-response models, the probit model being an exception.) Bailar et al. (19) show that a significant fraction of bioassays conducted for the National Toxicology Program demonstrate supra linearity at high experimental doses and argue that at low doses the one-hit model may thus not be conservative in some cases. Crump et al. (20), Peto (21), and Hoel (22) all argue that low-dose linearity occurs when substances augment existing carcinogenic processes. The formation of DNA adducts, which may be predictive of certain tumors induced by genotoxic carcinogens, has often been observed to be linear at very low doses (23,24). The question is thus not so much if low-dose linearity exists, but over what range the dose response is approximately linear. For the multistage model, Crump et al. (20) have shown that linear extrapolation will be quite accurate, at least when the excess risk does not exceed the spontaneous risk.

Tissue Dosimetry

Measurements or predictions of the dose of the proximate carcinogen reaching the target tissue can be used to obtain more accurate estimates of low-dose risks. This can be done using physiologically based pharmacokinetic (PBPK) models that describe the fate of chemical substances in the body (25). These models describe metabolic processes within a number of relevant physiological compartments and have been successfully used to model the metabolism of several chemical carcinogens (26).

When one or more steps in the process of metabolic activation are saturable, the dose delivered to the target tissue may not be directly proportional to the administered dose (27). In such cases, risk estimates based on the administered dose can be biased (28). At sufficiently low doses, however, most kinetic processes will be first-order, in which case the relationship between external and internal doses will be linear.

Linear Extrapolation

We have argued that dose-response curves for some carcinogens may be expected to be linear at low doses. If the dose-response curve is actually sublinear in the low-dose region, linear extrapolation provides an upper limit on low-dose risk. In this section, we first review previously proposed methods for linear extrapolation and then describe our model-free approach.

Previous Approaches

Gross et al. (29) suggested a method for linear model extrapolation based on discarding data starting at the upper end of the dose range until a linear model provided an adequate description of the remaining data. Van Ryzin (30) suggested the use of any model that fit the data reasonably well to estimate the dose producing an excess risk of 1% and then using simple linear extrapolation to lower doses. Gaylor and Kodell (31) proposed fitting a model to the available data and then using linear extrapolation below the lowest dose at which observations were taken. Since the estimates at the lower doses might be unduly influenced by the choice of the model used in the experimental dose range, Farmer et al. (32) suggested linear extrapolation below the lowest dose or the dose corresponding to an estimated risk of 1%, whichever was larger.

Krewski et al. (33) propose an entirely model-free procedure based on linear extrapolation below the lowest dose showing an excess (not necessarily statistically significant) risk. Krewski et al. (34) modified their procedure to consider linear extrapolation from all doses for which there were no statistically significant increases in tumor incidence above the baseline level, selecting the smallest slope for low-dose risk estimation. In a similar vein, Gaylor (35) considered the smallest slope obtained from all the possible combinations of data from the doses where the lowest dose was in the convex portion of the dose-response curve. In both cases, upper confidence limits on the slopes were used. Both Krewski et al. (33) and Gaylor (35) showed that low dose risk estimates based on these model-free procedures were generally close to those obtained from the linearized multistage model.

Model-Free Approach

The only assumption that we wish to entertain in assessing low-dose cancer risks is that of linearity of the dose-response curve at low doses. Under this assumption, low-dose risk assessment requires estimation of the slope of the dose-response at the origin given by

$$\beta = \frac{\partial P(d)}{\partial d} \bigg|_{d = 0} > 0 \quad (4)$$

Without making specific assumptions concerning the functional form of the dose-response curve other than low-dose linearity, a natural estimator of $\beta$ at a dose $d$ close to 0 would be the slope

$$\hat{\beta}_d = \frac{P(d) - P(0)}{d} \quad (5)$$

of the secant from $(d, P(d))$ to $(0, P(0))$, since $\hat{\beta}_d \rightarrow \beta$ as $d \rightarrow 0$. This approximation suggests a simple model-free approach to linear extrapolation.

Consider a bioassay with $t+1$ dose levels $0 = d_0 < d_1 < \ldots < d_t$ where $d_0 = 0$ corresponds to the control group. Of the $n_i$ animals at dose $d_i$, suppose that $x_i$ develop the lesion of interest during the course of the study ($i=0, 1, \ldots, t$). The probability $p_i$ of tumor development at dose $d_i$ may then be estimated by $\hat{p}_i = x_i/n_i$. Linear interpolation between a point $\hat{p}_i$ ($1 \leq i \leq t$) and $\hat{p}_0$ yields the secant approximation to the linear component of the dose-response curve.

To ensure that this approximation is reasonable, we need to restrict the set $[\hat{p}_1, \ldots, \hat{p}_t]$ to some subset $[\hat{p}_1, \ldots, \hat{p}_s]$ of points ($1 \leq s \leq t$) such that this subset lies within a region of the dose-response curve in which the secant approximations will not underestimate the low-dose slope. After smoothing the proportions so as to form a monotonically increasing set $[\hat{p}_s]$ using isotonic regression, Gaylor (35) selected $\hat{p}$ to correspond to the convex region of the dose-response curve. Schnoyer (36) used sigmoidal regression to smooth the dose-response curve, yielding a value of $\hat{p}$ up to which the smoothed proportions would be convex. Both of these smoothing procedures can notably alter observed proportions $[\hat{p}_s]$. Isotonic and sigmoidal regression also raise technical complications when confidence
limits on the smoothed proportions \( \hat{p}_i \) are considered (37).

Krewski et al. (34) adopted a simpler approach in which \( r^* \) was chosen to correspond to be the largest dose below the first dose at which the observed response rate among the exposed groups was significantly greater than the response in controls. (Here, statistical significance is evaluated at the 5% level using the Fisher–Irwin exact test.) If the lowest dose exhibits a statistically significant increase in tumors, only this dose is used for extrapolation. In this case, the results should be interpreted with caution since there is less assurance of convexity. To allow for experimental error, an exact binomial upper confidence limit \( p_i^{(0)} \) was calculated on \( p_i \) (\( i=1, \ldots , r^* \)), along with a lower confidence limit \( p_i^{(0)} \). The minimum (positive) value of the \( r^* \) secants \( (p_i^{(0)} - p_0^{(0)})/d_i, (i=1, \ldots , r^*) \) is then used as an upper confidence limit on the low-dose slope. Because no dose-response model has been assumed, we refer to this as model-free extrapolation (MFX).

Because the minimum of up to \( r \) such secants is selected, the overall confidence level associated with this procedure requires consideration. By the Bonferroni inequality, an overall 95% confidence level may be achieved using individual confidence limits of \( 5/(t+2) \% \). Since not all \( r \) secants are used when \( r^* < r \), it is possible that this Bonferroni bound may be improved upon. This is currently under investigation.

**Illustrative Examples**

To illustrate the application of the model-free approach to linear extrapolation, we consider the data on radiation-induced stomach cancer shown in Table 1, previously analyzed by Krewski et al. (34). These data are shown in graphical form in Figure 1A after re-expression in terms of relative risk. The secant bounds based on those exposure groups not demonstrating a significant increase in risk (\( p < 0.05 \)) are shown in Figure 1B. The secant with the smallest slope represents the MFX bound on low-dose risk.

To compare the MFX approach with the traditional LMS, consider the bioassay data shown in Table 2 on kidney tumors induced in Fischer 344 rats following oral exposure to nitrosotriacetic acid (NTA) for 24 months (38). These same data are displayed graphically in Figure 2A, along with the fitted multistage model (39). The best-fitting model involves five stages but does provide a good description of the dose-response curve.

The \( (100 - 5/6) = 99.17 \% \) upper confidence limits on the response probabilities in each of the exposed groups are shown in Figure 2B, along with the associated secant bounds on the low-dose slope. (No secant is shown for the dose of 2% NTA in the diet, since the tumor response at this dose was significantly greater than 0, the control response.) The minimum slope of these secants occurs at a dose of 1.5% and has a value of 0.061 per percent NTA in the diet.

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An upper confidence limit on the slope of the dose-response curve at the origin can also be derived under the LMS model. For comparability with MFX, this is calculated as $10^{-3/d^*}$, where $d^*$ represents a 95% lower confidence limit on the dose corresponding to an additional risk of 1% (39). (This differs slightly from $q^*$ when the background tumor response rate is not low.) This leads to a slope of 0.024, a factor of 2.5 lower than obtained with MFX.

**Empirical Evaluation**

The general performance of our model-free extrapolation (MFX) procedure in comparison with the traditional LMS may be empirically evaluated by applying both methods to experimental data on a more extensive series of test compounds. In this regard, Gold et al. (40-42) have assembled a useful reference database of bioassay data drawn from 3749 experiments reported in the literature. Here, an experiment is defined in terms of results for one sex of one species from one research report.

For our purposes, a subset of this database was selected for analysis. First, only data on rats, mice, and hamsters were considered to avoid studies with larger mammals such as dogs or monkeys in which exposure occurred over a relatively small fraction of their lifespan. Second, experiments in which exposure took place by more than one route were excluded because of pharmacokinetic complications arising with multiple exposure routes. Third, only experiments with at least two dose groups (in addition to the unexposed control group) were used in keeping with minimal standards of bioassay design. Fourth, experiments with reduced survival among exposed animals were excluded since this could bias tumor occurrence rates downward. (Using only low doses with MFX would help to alleviate this problem, as reduced survival generally occurs at higher doses.)

Experiments selected according to these criteria often included data on tumor occurrence at more than one site. Gross aggregations of sites (all target sites or tumor bearing animals) were excluded on the basis that most carcinogens appear to be site specific. Similarly, aggregations of all tumors at a given site were omitted. For our purposes, only the most significant site was considered, this being the site on which most concern would likely focus in practice. Here, significance was defined in terms of the $p$-value of the Cochran-Armitage test for increasing linear trend in tumor response with increasing dose (43). In cases where two or more sites had the same $p$-value, the one with the smallest TD$_{50}$ (the dose resulting in 50% tumor incidence) was selected. To ensure that compounds selected for analysis were considered in some sense to be carcinogens, only those results for which the (one-sided) $p$-value for the trend test was less than 1% were admitted. Additional evidence of carcinogenicity was required by further demanding an expressed opinion by the original investigators that the compound was considered carcinogenic.

Application of these criteria to the Gold database yielded 585 experiments for analysis. The slope of the dose-response curve at the origin was estimated using MFX and the LMS model. In the latter analyses, doses associated with a down turn in the dose-response curve at high doses were omitted. In 13 cases, the sample size limitations for MFX were exceeded. This left 572 experiments for comparison purposes.

The distribution of the ratios (MFX/LMS) of the two estimates across the 572 data sets is shown in Figure 3. The median ratio

**Figure 3.** Frequency distribution of ratios of estimates of low-dose slopes (MFX/LMS) based on 572 experiments.
was 1.3, indicating a tendency toward slightly higher slope estimates with MFX than with LMS. In 443 of 572 cases, the MFX estimate was within a factor of two of the LMS estimate. There were eight instances in which MFX exceeded LMS by a factor of more than 10-fold. A case-by-case examination of those cases revealed a leveling off or even a decrease in the dose-response curve at higher doses, which tended to reduce the value of $q_f$. Since MFX does not generally use high-dose data, a higher (and likely more accurate) estimate of the slope of the dose-response curve at low doses is obtained.

## Summary and Conclusions

The quantitative assessment of risks associated with low-level exposure to carcinogens present in the environment continues to be an important problem upon which consensus remains to be attained. This issue is particularly contentious when extrapolations not only from high to low doses but from laboratory animals to humans must be made. Nonetheless, such estimates are often needed for purposes of risk management.

The LMS model has traditionally been used for low-dose risk estimation. It is now widely recognized that this model provides an incomplete description of chemical and radiation carcinogenesis, neglecting important factors such as tissue growth and cell kinetics. Dose–response relationships demonstrating a high degree of curvature at high doses can occur as a result of cellular proliferation or saturation of metabolic processes required to form the proximate carcinogen, but can be explained only with a large number of stages in the multistage model. Although more biologically based models have emerged within the last decade, these models involve additional unknown parameters that may not be directly estimable using epidemiological or toxicological data on tumor occurrence rates.

Irrespective of the actual dose-response model, there are a number of arguments that suggest that the dose-response curve may be linear at low doses. Specifically, low-dose linearity may be expected to hold with agents that act by augmenting ongoing carcinogenic processes. DNA adducts formed with genotoxic carcinogens also appear to be linearly related to dose at low levels of exposure.

For these reasons, a model-free approach to carcinogenic risk assessment that assumes nothing more than low-dose linearity seems appealing. The model-free extrapolation (MFX) procedure described in this article is based on a series of secant approximations to the slope of the dose-response curve in the low-dose region, with the minimum of such approximations selected for risk assessment purposes. This represents the best upper confidence limit on low-dose risk consistent with the data.

An analysis of 572 experiments demonstrated that MFX yields estimates of low-dose risk are largely comparable to estimates derived under the LMS model. In addition to making a minimal number of assumptions, MFX does not make use of data at high doses where survival may be impaired or normal physiological function disrupted.

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