Hydrodynamic properties of cyclodextrin molecules in dilute solutions

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Abstract Three well-known representatives of the cyclodextrin family were completely characterized by molecular hydrodynamics methods in three different solvents. For the first time the possibility of an estimation of velocity sedimentation coefficients \( s \) between 0.15 and 0.5 S by the numerical solution of the Lamm equation is shown. Comparison of the experimental hydrodynamic characteristics of the cyclodextrins with theoretical calculations for toroidal molecules allows an estimation of the thickness of the solvent layers on the surface of cyclodextrin molecules.

Keywords Cyclodextrins · Molecular hydrodynamics · Toroid

Introduction

Cyclodextrins (CDs) are well-known objects of supramolecular chemistry and glycoscience (Dodziuk 2006; Philp and Stoddart 1996; Szejti and Osa 1996; Wenz 1994). They are products of amyllopectin enzymatic destruction by the action of extracellular enzymes, cyclodextrin glycosyltransferases (CGTase, E.C. 2.4.1.19) (Qi and Zimmermann 2005). The more abundant and available of the CDs are cyclic oligosaccharides, consisting of 6, 7, 8 D-glucose residues, connected with \( \alpha (1 \rightarrow 4) \) links and named \( \alpha-\), \( \beta-\) and \( \gamma-\)CD, respectively. The shape of these molecules resemble a hollow truncated cone with a central cavity, containing C3H and C5H carbons atoms and ester-like O-4 and O-5 oxygen atoms. The CD structure provides an external hydrophilic region and a rather hydrophobic inner cavity (Bender and Komiyama 1978). The number of sugar rings defines the size of the cavity and the flexibility of the CDs. CDs and their derivatives are well-known as molecular hosts capable of including, in their cavities, different guest molecules of appropriate size, shape, and polarity via non-covalent interactions (Connors 1997; Dodziuk 2006; Harada 1997; Saenger 1980; Szejti 2004). The apolar nature of their cavities (Harada 1997) allows CDs to act as hosts preferentially for nonpolar guests, which include small molecules and surfactants (Harada 1997; González-Pérez et al. 2008). The interactions of CDs with natural and synthetic polymers bearing attached hydrophobic tags have also been intensively studied (Beheshti et al. 2006; Burckbuchsler et al. 2006; Charlot et al. 2006; Rinaudo et al. 2005; Sabadini and Cosgrove 2003). In addition, CD...
derivatives are being used as a core in the synthesis of star-like polymer systems (Hoogenboom et al. 2006). Cyclodextrins’ ability to form inclusion complexes with appropriate sized hydrophobic guest molecules is the most frequently applied property of CDs (Hedges 1998; Szejti 2004) and has been studied by spectroscopic, kinetic, and crystallographic methods (Dodziuk 2006; Saenger et al. 1998; Szejti and Osa 1996). CDs and their derivatives are considered to be potential carriers for hydrophobic pharmaceutical compounds (Loftsson and Duchene 2007; Uekama et al. 1998). However, information about the properties of cyclodextrins molecules in diluted solution is still rather scarce (Dodziuk 2006; Nakata et al. 2003; Longsworth 1953; Szejti 1998).

In this study, we present investigations on α-, β- and γ-cyclodextrin by macromolecular hydrodynamics.

**Materials and methods**

The CDs studied, α-, β- and γ-cyclodextrin, were obtained commercially from Sigma (purity ≥ 98%) (Table 1). Velocity sedimentation, the translational diffusion, and viscosity as well as the increment of density were measured in three different solvents: water, dimethylformamide, and dimethylsulfoxide.

Sedimentation velocity experiments were performed on a Beckman XLI analytical ultracentrifuge at a rotor speed of 55,000 rpm and at 20°C in Al-double-sector cells of optical path 12 mm using interference optics. The evaluation program Sedfit for continuous particle size distributions (Schuck 2000) was used for data analysis. The regularization method used was the Tikhonov-Philips 2nd derivative, and the confidence level (F ratio) chosen was 0.8–0.9. By fitting for (ffsph) in a nonlinear regression, an estimate of the weight-average frictional ratio of all macromolecules in solution is obtained, where f is the frictional ratio of the solute macromolecule and fsph is the frictional ratio of the rigid sphere with the same “anhydrous” volume (free of solvent) as the macromolecule. The final result is the differential distribution (dc(s)/ds) of the sample, which is named c(s). It is scaled such that the area under the c(s) curve between the smallest s value, s1, and the largest one, s2, in the distribution will give the loading concentration of macromolecules between these sedimentation coefficients (expressed in number of fringes, J, in the case of interference optics). J, which is proportional to the polymer concentration in solution, was used to calculate

| CD          | Images of modeling structures | M (g/mol) | dii (10⁻⁸ cm) | do (10⁻⁸ cm) | M (MALDI) (g/mol) |
|-------------|------------------------------|----------|---------------|--------------|-------------------|
| α-CD (C₆H₁₀O₅)₆ | ![α-CD](image1)                | 972.9    | 5.0–4.7       | 14.6         | 972.4             |
| β-CD (C₆H₁₀O₅)₇ | ![β-CD](image2)               | 1,135.0  | 6.5–6.0       | 15.4         | 1,134.5           |
| γ-CD (C₆H₁₀O₅)₈ | ![γ-CD](image3)               | 1,297.1  | 8.3–7.5       | 17.5         | 1,296.6           |

* As measured on space-filling or CPK models (Saenger 1980; Corey and Pauling 1953)
the refractive index increment: \( \Delta n/\Delta c = J^0/kC_1 \) (Pavlov et al. 2003), where \( \lambda \) is the wavelength (675 nm), \( K \) the magnifying constant and \( l \) the optical path. With \( K = 1 \) and \( l = 12 \) mm we obtain: \( \Delta n/\Delta c = 5.625 \times 10^{-3} (J/c) \) and \( c \) in g/cm³.

Translational diffusion was studied by the classical method of forming a boundary between the solution and the solvent on Tsvetkov polarizing diffusiometer (Tsvetkov 1989). The diffusion boundary was formed in glass cell of length \( h = 30 \) mm along the beam path. The optical system used for recording the solution-solvent boundary in diffusion analysis was a Lebedev’s polarizing interferometer (Lebedev 1930). Translational diffusion coefficients were calculated from the equation:

\[
\sigma^2 = \sigma_0^2 + 2Dt,
\]

where \( \sigma^2 \) is the dispersion of the diffusion boundary calculated from the maximum ordinate and the area under the diffusion curve, \( \sigma_0^2 \) is the zero dispersion characterizing the quality of boundary formation, and \( t \) is the diffusion time. Experiments were carried out at 25°C, and the intrinsic diffusion coefficient, which depends only on the macro-molecule properties, is calculated as: \( [D] = D_0\eta_0/T \).

Viscosity measurements were conducted using an Ostwald viscometer. The respective flow times, \( \tau_0 \) and \( t \), were measured at 25°C for the solvent and polymer solutions, with relative viscosities \( \eta_r = \rho / \rho_0 \). The extrapolation to zero concentration was made by using both the Huggins and Kraemer equations (Cantor and Schimmel 1980; Tsvetkov 1989) and the average values were considered as the value of intrinsic viscosity.

The density measurements were carried out in the density meter DMA 5000 (Anton Paar, Graz, Austria) according to the procedure of Kratky et al. (1973).

The cyclodextrins were investigated also by Matrix-Assisted Laser Desorption/Ionisation Time-Of-Flight Mass Spectrometry (MALDI-TOF MS). MALDI-TOF MS measurements were performed with an Ultraflex III TOF/TOF (Bruker Daltonics, Bremen, Germany) equipped with a Nd:YAG laser and a collision cell. All spectra were measured in the positive reflector mode. For the MS/MS mode, argon was used as collision gas at a pressure of 2 \( \times 10^{-6} \) mbar. The instrument was calibrated prior to each measurement with an external PMMA standard from PSS Polymer Standards Services GmbH (Mainz, Germany) in the required measurement range. MS and MS/MS data were processed using PolyTools 1.0 and an isotope pattern calculator.

Results and discussion

The velocity sedimentation and isothermal translational diffusion studies were made separately in three different solvents: water, dimethylformamide (DMF) and dimethyl-sulfoxide (DMSO). The solubility of the CDs studied in these solvents increases in the following order: \( H_2O < DMF < DMSO \). The velocity sedimentation experiments were run overnight (12–14 h), at a solute concentration \( c \approx 4 \) mg/mL. Figure 1 represents the sedimentation interference profiles of \( \gamma \)-cyclodextrin in DMF and in DMSO as well as the calculated distribution of the sedimentation coefficients, \( c(s) \), as obtained by the use of the Sedfit program. Figure 2 shows the comparison of the normalized differential distributions for \( \gamma \)-CD, obtained in the different solvents. The density increment (\( \Delta n/\Delta c \)), which is also required for the quantitative interpretation of the sedimentation data, allows the determination of the partial specific volume (ii). The value remained the same for different CDs in the same solvent and was found to be 0.667, 0.632, and 0.649 cm³/g in \( H_2O \), DMF, and DMSO, respectively. The refractive index increment (\( \Delta n/\Delta c \)) also remained virtually the same for different CDs in the same solvent: 0.148, 0.104, and 0.07 cm³/g in \( H_2O \), DMF, and DMSO, respectively. The translational diffusion was studied at an average solute concentration \( c \approx 1–2 \) mg/mL (Fig. 3).

The values of both the sedimentation coefficient \( s \) and the diffusion coefficient \( D \) obtained at the concentrations given above were assumed to be equal to the values extrapolated to zero concentration. The solute concentrations practically correspond to the limiting dilution as the values of the Debye parameter \( c(\eta) \), describing dilution of a solution, is within the limits of 0.01 \( \leq c(\eta) \leq 0.03 \). The plots of \( \eta_s/c \) and \( \ln \eta/c \) as a function of \( c \) allowed us to determine the intrinsic viscosity, \( [\eta] \), of the cyclodextrins (Fig. 4). Table 2 represents the values of \( s, (f f_{sp}) \), \( D \), and \( [\eta] \) obtained.

The different experimental hydrodynamics measurements can be expressed as intrinsic values, \( [\eta] \), \( [s] \), \( [D] \), \( [f] \), which are independent of the solvent properties (Cantor and Schimmel 1980; Tsvetkov 1989). Each of them is related to common macromolecular characteristics such as molar mass \( M \) and mean-square radius of gyration \( <R^2> \):

\[
[\eta] = \Phi' <R^2> ^{3/2}/M
\]

\[
[s] \equiv s_0\eta_0/(1 - \rho_0v) = M/N_A\Phi' <R^2> ^{1/2}
\]

\[
[D] \equiv D_0\eta_0/T = k/[f] = k/P' <R^2> ^{1/2}
\]

\[
[f] \equiv f_0/\eta_0 = P' <R^2> ^{1/2}
\]

with \( [\eta] \): intrinsic viscosity; \( [s] \), \( [D] \), and \( [f] \): intrinsic coefficients of velocity sedimentation, translational diffusion, and translational friction, correspondingly; \( N_A \) is the Avogadro number, and \( \Phi' \) and \( P' \) are the Flory hydrodynamic parameters. These relationships have a general meaning and are valid for any type of molecules/
macromolecules. The values of the dimensionless parameters $U_0$ and $P_0$ depend, however, on the shape and asymmetry of the solute molecules and, in addition, on the hydrodynamic interactions between the different parts of the same molecule which exercise the friction in the liquid medium. The theoretical values of these parameters are obtained by solving the hydrodynamic problem and depend on the models and mathematical approximations.

A frequently used concept in biochemistry and polymer science is that of the hydrodynamic equivalent sphere. In this concept, the real molecule is modeled by a rigid sphere which has the same translational frictional coefficient. The radius of the hydrodynamic equivalent sphere is calculated from the Stokes relation (5'). In the case of the intrinsic viscosity the Einstein relation (2') is applied.

$$[\gamma]_{\text{sph}} = 6\pi R_{\text{sph}}$$

$$[\eta]_{\text{sph}} = \left(\frac{10}{3}\pi N_A\right)\frac{R_{\text{sph}}^3}{M}$$

Obviously the radius of a hydrodynamic equivalent sphere can differ considerably from the size of the real molecule. Nevertheless, this approach is useful, in
particular when sizes in a series of polymerhomologues are to be compared, e.g., for proteins, dendrimers, or highly branched macromolecules.

Combination of Eqs. 3 and 4 leads to the Svedberg equation (Cantor and Schimmel 1980; Maechtle and Boerger 2006; Tsvetkov 1989) used for molar mass determination from the hydrodynamic data:

$$M_{sd} = \frac{(RT)/(1-vp_0))(s_0/D_0)}{(N_A/(1-vp_0))s_0f_0}$$  \hspace{1cm} (6)

The translational friction coefficient $f_0$ of molecules may be expressed in our case by the following way:

$$f_0 = (f/f_{sph})_0f_{sph} = (f/f_{sph})_0\frac{6\pi n_0(3Mv_bar/4\pi N_A)^{1/3}}{9}$$  \hspace{1cm} (7)

From the Eqs. 4 and 7 it is possible to calculate the translational diffusion coefficients and, correspondingly, the intrinsic translational diffusion coefficient:

$$[D]_{df} = k \times (9\pi 2^{1/2})^{-1} \left( \frac{f/f_{sph}}{s_0} \right)_{0}^{-3/2} \left( \frac{[s]v}{\nu} \right)^{-1/2}$$  \hspace{1cm} (8)

Linking $s_0$ and $[D]_{df}$ in the equation obtained from Eqs. 6 and 8 allows us to determine the molar mass of moving molecules using:

$$M_{df} = 9\pi 2^{1/2}N_A\left( \frac{[s]}{f/f_{sph}} \right)_{0}^{3/2} v^{1/2}$$.  \hspace{1cm} (9)

This equation is the transformation of original Svedberg equation 6 which, in turn, when $f/f_{sph} = 1$ is transformed into the relationship describing the solid sphere model.

Table 3 shows the molar masses and hydrodynamic radii of the CDs studied, as determined from the experimental data by use of the equations given above.

Comparison with the $M$ values calculated from the chemical structure of the CDs shows that, in all solvents, the experimental data are relatively close to the theoretical ones. The measurements in DMF yield by far the closest agreement, the deviations being below 10% for all samples. But even for the worst result, obtained with γ-CD in DMSO, the deviation is below 50%. These results are highly surprising, since the $s$ values on which they are based are around 0.5 S or even, in the solvent DMSO, around 0.15 S. As far as we know, the possibility of correctly or nearly correctly determining such small velocity sedimentation coefficients on the basis of the numerical solution of the Lamm equation has not been demonstrated before. It should be noted that, in the experiments described, the evolution of the sedimentation boundary occurs without appreciable boundary displacement. Elementary estimation shows that when the sedimentation coefficient is only 0.1 S the shift of the sedimentation boundary during 12 h of experiment at 55,000 rpm amounts to only 1 mm. To fix this shift by usual methods against a background of significant diffusion spreading obviously is not possible. In order to further strengthen the conclusions described,
Table 2 Translational diffusion coefficient $D$, velocity sedimentation coefficient $s$, frictional ratio $f/f_{qph}$ and intrinsic viscosity $[\eta]$, of CD in H$_2$O, DMF, and DMSO

|        | H$_2$O     | DMF    | DMSO    |
|--------|------------|--------|---------|
|        | $10^7D$ (cm$^2$/s) | $s$ (S) | $f/f_{qph}$ | $[\eta]$ (cm$^3$/g) | $10^7D$ (cm$^2$/s) | $s$ (S) | $f/f_{qph}$ | $[\eta]$ (cm$^3$/g) | $10^7D$ (cm$^2$/s) | $s$ (S) | $f/f_{qph}$ | $[\eta]$ (cm$^3$/g) |
| $\alpha$ | 36.5       | 0.48   | 1.00    | 34            | 0.49       | 1.33    | 5.5    | 9.7           | 0.15       | 1.38    | 5.4    |
| $\beta$  | 29.1       | 0.51   | 1.00    | 29            | 0.53       | 1.33    | 5.2    | 8.2           | 0.11       | 1.43    | 6.0    |
| $\gamma$ | 27         | 0.53   | 1.06    | 25.5          | 0.58       | 1.37    | 5.9    | 8.45          | 0.18       | 1.49    | 7.5    |

Table 3 Molar mass (g/mol) and hydrodynamic radii $R_0 \times 10^9$ cm ($\pm 9\%$) of CD in different solvents

|        | H$_2$O     | DMF    | DMSO    | $M_{av}$ |
|--------|------------|--------|---------|----------|
|        | $M$       | $R_0$ | $M$     | $R_0$    | $M$     | $R_0$ |
| $\alpha$ | 1,100      | 6.7    | 970     | 8.2      | 1,300   | 10     | 1,100 $\pm$ 100 |
| $\beta$  | 1,300      | 7.7    | 1,150   | 9.1      | 1,100   | 11     | 1,180 $\pm$ 80 |
| $\gamma$ | 1,500      | 8.5    | 1,400   | 10.1     | 1,900   | 12.4   | 1,600 $\pm$ 200 |

we have checked the validity of the theoretical $M$ values by MALDI-TOF. The experimental spectra are presented in Fig. 5. Taking into account the mass of sodium ion the good correlation is observed between calculated and experimental values of molar masses (Table 1).

The average values for the radii of the hydrodynamic equivalent sphere, calculated from the Stokes ($5'$) and Einstein (2') relationships are also presented in Table 3. These values characterize certain external sizes of CDs molecules. When comparing these data with those measured on space-filling or CPK models (Table 1, $r_0^{CPK} \approx d_{ol}$/2) (Saenger 1980; Corey and Pauling 1953), it is interesting to note that (1) both kinds of radii virtually agree in water, and (2) the ratios of the hydrodynamic to the radii $r_0^{CPK}$ remain virtually constant in the series of studied CDs but vary in different solvents: $R_{H_2O}/r_0^{CPK} = 0.96 \pm 0.03 \approx 1.0$, $R_{DMF}/r_0^{CPK} = 1.15 \pm 0.02$, and $R_{DMSO}/r_0^{CPK} = 1.41 \pm 0.02$. Since hydrodynamic interactions inside of CDs molecules will contribute to the friction of the molecules, different ratios of radii in different solvents may reflect not only different sizes but also different hydrodynamic interactions.

A more adequate model for the description of the hydrodynamic behavior of CDs molecules can be toroidal particles/molecules. In recent years approaches which aimed at modeling the shape of biopolymers by bead-shell models were extended to the calculation and predictions of biopolymer hydrodynamic properties (Garcia de la Torre and Bloomfield 1977, 1981; Allison 1999; Garcia de la Torre 2001). Applying such methods to toroids, the dependency of the translational diffusion coefficient and of the intrinsic viscosity on the characteristic ratio of toroids, $x = r_l/r_0$, was derived ($r_l$, $r_0$: inner and outer radius, respectively) (Garcia de la Torre 2001). The following interpolating polynomials were obtained for dimensionless values $[D]r_0/k$ and $0.01[\eta]M/(N_Ar_0^3)$:

$$[D]r_0/k = 0.0620 - 0.00143x + 0.0278x^2$$ (10)

$$0.01[\eta]M/(N_Ar_0^3) = 0.0701 - 0.0365x - 0.0629x^2$$ (11)

A comparison of the experimental and computational results is shown in Fig. 6. As a first approximation, the space-filling models or CPK models data were used to characterize the outer and inner sizes of the CD molecules (Saenger 1980; Szejti 1998). The details of the deviation of the experimental points from the theoretical curves correlate to the above-obtained estimations concerning the hydrodynamic radii of the CD molecules in different solvents. In the plots shown, $r_0$ is the more crucial parameter since the ordinate directly depends on it whereas the dependence on $r_l$ becomes apparent only as a ratio of $r_l/r_0$ in the abscissa. Both plots indicate that, in order to superimpose the experimental data to the computational results, it is necessary to increase the outer sizes of CD molecules. In practice, these sizes could be increased in solution by the absorption of a few solvent molecules to the external surface of the CD molecules, forming an absorbed layer. Thus, in solution the outer size of CD molecules may be characterized by an effective radius $r_0^{eff} = r_0 + \Delta r_0$, where $\Delta r_0$ is the average thickness of solvent layer. The latter figure probably correlates to the size and the number of the solvent molecules. The size of the solvent molecules can be estimated by the relationship $d = (6M/\pi\rho_0N_A)^{1/3}$. 3.86, 6.26, and 6.08 $\times 10^{-8}$ cm for H$_2$O, DMF, and DMSO molecules were obtained, respectively. The calculated results could be fitted to the experimental ones by assuming that the thickness of the solvent layer varies depending on the solvent, amounting for $\Delta r_0 \approx 0.5d_{solv}$ in water and DMF but $\Delta r_0 \approx d_{solv}$ in DMSO. These layers are formed by different numbers of solvent molecules. Qualitatively the number of DMSO molecules must be higher in comparison with both other solvents.

Although, in reality, the CD structure in solution are flexible, whereby CD instant conformations probably differ from each other because of a variation of the valence...
Fig. 5 MALDI-TOF-MS spectrum for the cyclodextrins (1 α-CD, 2 β-CD, 3 γ-CD) obtained on dihydroxybenzoic acid as matrix and NaTFA as a source of sodium ions. The figures at the peaks are the molar masses of cyclodextrine isotopes including the mass of one sodium ion.

Fig. 6 Comparison of experimental hydrodynamic values (1–3) with the calculated hydrodynamic values for toroidal molecules (4): a characteristic translational diffusion coefficient (1, 1: in H2O, 2, 2: in DMF, 3, 3: in DMSO) b intrinsic viscosity (1, 1: in DMF, 2, 2: in DMSO) (1–3): The hydrodynamic values are plotted in function of the space-filling (or CPK) models radii rCPK (average inner) and rCPK (outer) of the CD molecules (Table 1). (1′–3′): The hydrodynamic values are plotted in function of effective outer radii r0eff (see text).
angles of the glycosidic links and, possibly, a twist-conformation of the sugar rings (French and Johnson 2007; Saenger et al. 1998). Nevertheless, the CD time-average characteristics, as monitored by hydrodynamic methods, can be fully interpreted by a rigid toroid model.

Conclusion
The velocity sedimentation and translational diffusion coefficients of CD molecules were measured in water, DMF, and DMSO. In DMF and DMSO also the intrinsic viscosities could be measured. It was possible to determine from the hydrodynamic data, by use of the Sedfit program, relatively accurate values for CD molar mass and size, despite the fact that the sedimentation coefficients were as low as 0.1–0.5 S. The correspondence of the CD hydrodynamic values with the results calculated for toroids by use of a bead-shell model is demonstrated. This comparison also shows that the outer CD dimensions are solvent-dependent and larger than those obtained from the crystallographic data.

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References
Allison SA (1999) Low Reynolds number transport properties of axisymmetric particles employing stick and slip boundary conditions. Macromolecules 32:5304–5312. doi:10.1021/ma990579c
Beheshi N, Bu H, Zhu K, Kjøniksen A-L, Knudsen KD, Pannies R, Hernández-Cifre JG, García de la Torre J, Nyström B (2006) Characterization of interactions in aqueous solutions of hydroxyethylcellulose and its hydrophobically modified analogue in the presence of a cyclodextrin derivative. J Phys Chem B 110:6601–6608. doi:10.1021/jp050682v
Bender ML, Komiyama M (1978) Cyclodextrin chemistry. Springer, Berlin
Burckbuehler V, Kjøniksen A-L, Galant C, Lund R, Amiel C, Knudsen KD, Nyström B (2006) Rheological and structural characterization of the interactions between cyclodextrin compounds and hydrophobically modified alginate. Biomacromolecules 7:1871–1878. doi:10.1021/bm060149o
Cantor CR, Schimmel PR (1980) Biophysical chemistry, vol 1. Freeman, San Francisco
Charlot A, Heyraud A, Guenot P, Rinaudo M, Auzely-Velty R (2006) Controlled synthesis and inclusion ability of a hyaluronic acid derivative bearing z-cyclodextrin molecules. Biomacromolecules 7:907–913. doi:10.1021/bm0507094
Connors KA (1997) The stability of cyclodextrin complexes in solutions. Chem Rev 97:1325–1357. doi:10.1021/cr960371r
Corey RB, Pauling L (1953) Molecular models of amino acids, peptides, and proteins. Rev Sci Instrum 24:621–627. doi:10.1063/1.1770803
Dodziuk H (ed) (2006) Properties and application of cyclodextrins: cyclodextrins and their complexes. Wiley, USA
French AD, Johnson GP (2007) Linkage and pyranosyl ring twisting in cyclodextrins. Carbohydr Res 342:1223–1237. doi:10.1016/j.carres.2007.02.033
García de la Torre J (2001) Building hydrodynamic bead-shell models for rigid biopolymers of arbitrary shape. Biophys Chem 94:265–274. doi:10.1016/S0301-4622(01)00244-7
García de la Torre J, Bloomfield VA (1977) Hydrodynamic properties of macromolecular complexes. Biopolymers 16:1747–1763. doi:10.1002/bip.1977.360160811
García de la Torre J, Bloomfield VA (1981) Hydrodynamic properties of complex, rigid, biological macromolecules, theory and applications. Q Rev Biophys 14:81–139
González-Pérez A, Dias RS, Nylander T, Lindman B (2008) Cyclodextrin-surfactant complex: a new route in DNA decompaction. Biomacromolecules 9:772–775. doi:10.1021/bm7012907
Harada A (1997) Design and construction of supramolecular architectures consisting of cyclodextrins and polymers. Adv Polym Sci 133:140–191
Hedges AR (1998) Industrial applications of cyclodextrins. Chem Rev 98:2035–2044. doi:10.1021/cr970141w
Hoogenboom R, Moore BC, Schubert US (2006) Synthesis of star-shaped poly(ε-caprolactone) via “click” chemistry and “supramolecular click” chemistry. Chem Commun (Camb) 4010–4012. doi:10.1039/b608313g
Kraaty O, Leonold H, Stahinger H (1973) The determination of the partial specific volume of proteins by the mechanical oscillator technique. Methods Enzymol 27:98–110. doi:10.1016/S0076-6879(73)27007-6
Lebedev AA (1930) L’interféromètre a polarisation et ses applications. Rev Opt 9:385–409
Loftsson T, Duchene D (2007) Cyclodextrins and their pharmaceutical applications. Int J Pharm 329:1–11. doi:10.1016/j.ijpharm.2006.10.044
Longsworth LG (1953) Diffusion measurements of aqueous solutions of amino acids, peptides and sugars. J Am Chem Soc 75:5705–5709
Maechtle W, Boerger L (2006) Analytical ultracentrifugation of polymers and nanoparticles. Springer, Berlin
Maedchle W, Boerger L (2006) Analytical ultracentrifugation of polymers and nanoparticles. Springer, Berlin
Nakata Y, Amitani K, Noriesue T, Kitamura S (2003) Translational diffusion coefficient of cycloamylose in aqueous sodium hydroxide. Biopolymers 69:508–509
Pavlov G, Finet S, Tatarenko K, Korneeva E, Ebel C (2003) Conformation of heparin studied with macromolecular hydrodynamic methods and X-ray scattering. Eur Biophys J 32:437–449. doi:10.1007/s00249-003-0316-9
Philip D, Stoddart JF (1996) Self-assembly in natural and unnatural systems. Angew Chem Int Ed 35:1154–1196. doi:10.1002/anie.199611541
Qi Z, Zimmermann W (2005) Cyclodextrin glucanotransferase: from gene to application. Appl Microbiol Biotechnol 66:475–485. doi:10.1007/s00253-004-1781-5
Rinaudo M, Auzely R, Vallin C, Mullagaliev I (2005) Specific interactions in modified chitosan systems. Biomacromolecules 6:2396–2407. doi:10.1021/bm0508005
Sabadini E, Cosgrove T (2003) Inclusion complex formed between chitosan and p-cyclodextrin-surfactant complex: a new route in DNA decompaction. Carbohydr Res 342:1223–1237. doi:10.1016/j.carres.2007.02.033
Saenger W (1980) Cyclodextrin inclusion compounds in research and industry. Angew Chem Int Ed Engl 19:344–362. doi:10.1002/anie.198003441
Saenger W, Jacob J, Gessler K, Steiner T, Hoffmann D, Saube H, Koizumi K, Smith SM, Tanaka T (1998) Structure of the common cyclodextrins and their larger analogues—beyond the doughnut. Chem Rev 98:1787–1802. doi:10.1021/cr9700181
Schuck P (2000) Size-distribution analysis of macromolecules by sedimentation velocity ultracentrifugation and Lamm equation modeling. Biophys J 78:1606–1619
