EVALUATION OF THE SURFACE HARDNESS OF COMPOSITE RESINS BEFORE AND AFTER POLISHING AT DIFFERENT TIMES

ABSTRACT

Purpose: The aim of this study was to evaluate the surface hardness of six composite resins: Revolution, Natural Flow, Fill Magic Flow, Flow-it! (flowables), Silux Plus (microfilled) and Z100 (minifilled) before and after polishing at different times. Materials and Methods: For this purpose, 240 specimens (5mm diameter, 1.4mm high) were prepared. Vickers hardness was determined before and after polishing at different times: immediately, 24h, 7 and 21 days after preparation of the samples. Statistical analysis was performed by ANOVA and Tukey test. Results: There was no difference in the hardness of flowable resins, which had lower hardness than the minifilled resin. The minifilled resin showed the highest surface hardness as compared to the other materials (p<0.01). All materials exhibited higher hardness after polishing, being more evident after 7 days. Conclusion: It may be concluded that, regardless of the composite resin, surface hardness was considerably increased when polishing was delayed and performed 1 week after preparation of the samples. Uniterms: Hardness; Composite resins; Polishing.
INTRODUCTION

After shaping and polymerization, the surface of a dental composite restoration will normally remain rough28. Surface roughness allows plaque accumulation29, which may result in gingival inflammation, superficial staining and secondary caries. Proper surface finishing and polishing are critical clinic procedures, which enhance esthetics and longevity of restorations. Moreover, polishing reduces roughness and scratches created by finishing instruments30.

Although the esthetic restorative materials that are light-cured against a matrix strip are not devoid of imperfections, they present the smoothest surface that is possible to achieve1,24. However, previous studies10,24 showed that hardness values for the celluloid strip-finished composites were lower than those of polished surfaces, probably due to the accumulation of organic matrix on the surface.

Since their introduction, composite resins have been continuously developed in an attempt to improve their properties and broaden their clinical applications. The properties of composite resins can be altered by variations in composition and amount of resin matrix, as well as size and distribution of filler particles2,5-8,15,18,25-27. The greatest inorganic filler content is present in traditional minifilled composites with the intention of increasing hardness and wear resistance3,17.

Microfilled composite resins contain small filler particles and little amount of filler, which improve surface smoothness and the quality of polishing21. In the last decade, a new concept of composite resin, the flowable composite resin, was introduced in the dental market. This material presents modifications in viscosity and modulus of elasticity. Nevertheless, few researches about the influence of polishing intervals on surface hardness of flowable composites were reported. Considering this lack of information, the aim of the present study was to assess in vitro the surface hardness of flowable composite resins before and after polishing at different times, as compared to a microfilled and a minifilled composite resin.

MATERIALS AND METHODS

For this study, six composite resins were used: Revolution, Natural Flow, Fill Magic Flow, Flow-it! (flowable composites), Silux Plus (microfilled composite) and Z100 (minifilled composite). The tested materials and their manufacturers and characteristics are displayed in Table 1.

A total of 240 specimens were prepared – 40 per material and 10 for each tested interval. Initially, polyester resin cylinders with ¼ inch diameter and 10 mm high were obtained. The cylinders were finished with #280 to #400-grit silicon carbide paper to obtain a flat surface. Then, cavities (1.4mm deep 5mm in diameter) were prepared in the middle of cylinders with a wheel-shaped #4054 diamond bur.

The tested materials were inserted into the cavities in a single increment. A transparent polyester matrix strip was positioned on the material/cylinder surface and then a glass slide was gently pressed to obtain a flat and smooth surface. Each material was cured for 40 sec with a visible light-curing unit with 500mW/cm² output (XL 3000, 3M Dental Products, St. Paul, MN, USA) following the manufacturers’ instructions.

Vickers hardness (VHN) was evaluated using a micro-indentation tester (HMV-2, Shimadzu Co., Kyoto, Japan). For each specimen, three indentations were accomplished with a 50g load applied for 30sec, and the means were calculated in VHN. Measurements were recorded at different times: immediately, 24 hours, 7 days and 21 days after preparation of the samples, before and after polishing.

| Material        | Manufacturer          | # Batch Number | Filler                                      | % (vol) | Filler Size (µm) |
|-----------------|-----------------------|----------------|---------------------------------------------|---------|------------------|
| Revolution      | Kerr Corp. Orange, CA, USA | 905255         | Barium glass, synthetic silica              | 55%     | 1.0              |
| Natural Flow    | DFL Ind. e Com. Ltda. Rio de Janeiro, RJ, Brazil | 9908730        | Boron-aluminum silicate glass, synthetic silica | 43%     | ns               |
| Flow It!        | Jeneric-Pentron Inc. Wallinford, CT, USA | 26653          | Barium-boron-fluor-silicate glass           | 55%     | 1.5              |
| Fill Magic Flow | Vigodent S/A Ind. e Com. Rio de Janeiro, RJ, Brazil | 01199          | Barium aluminum silicate                    | ns      | 0.7              |
| Silux Plus      | 3M Dental Products St. Paul, MN, USA | 19990915       | Colloidal silica                            | 40%     | 0.04             |
| Z100            | 3M Dental Products St. Paul, MN, USA | 9GM            | Zirconia-silica                             | 70%     | 0.7              |

ns–not supplied by the manufacturer.
Specimens were stored in distilled water at 37ºC. For standardization, polishing was performed by the same operator using Super-Snap disks (Shofu Inc., Kyoto, Japan) in decreasing abrasive order, each one applied for 10 seconds.

Data were submitted to statistical analysis using three-way ANOVA and Tukey test at 0.05 significance level.

**RESULTS**

The means and standard deviations, before and after polishing, of all study groups are shown in Table 2.

The analysis of factors showed significant differences among composite resins, polishing and time. For the factor composite resins, it can be observed that, although the flowable composite resins yielded the lowest means, no statistically significant difference was observed among the different trademarks. Z100 minifilled composite showed statistically higher hardness values than the other tested materials (p<0.01), irrespective of time and polishing. Silux microfilled composite provided higher hardness (p<0.01) than the flowable composites. Comparing the composite resins and time, it can be verified that Silux showed similar behavior than Fill Magic for 24h.

The factor polishing influenced the hardness of all tested materials (p<0.01). Therefore, in general, polishing provided an increase in microhardness. When the different polishing intervals were analyzed, the interaction of composite resins and time, using the Tukey test, showed a gradual and statistically significant increase (p<0.05) in surface hardness. In the overall analysis of data, the highest hardness values were reached when polishing was accomplished 7 days after preparation of specimens, except for the Fill Magic Flow.

**DISCUSSION**

Hardness determines the degree of deformation of a material and it is generally accepted as an important property and a valuable parameter of comparison with the tooth structure. Changes in this property can be ascribed to the polymerization or maturation status of restorative materials. Enamel and dentin Vickers hardness values were stated as 348 VHN and 80 VHN, respectively.

To assure an optimized clinical performance of restorations, it is of paramount importance to employ materials with hardness at least similar to that of the dentinal substrate, not only superficially, but also in depth, since an accentuated decrease in hardness would adversely affect their mechanical properties and marginal integrity. In the present work, a gradual and significant increase in surface hardness was observed with regard to time, but regardless of the accomplishment of polishing.

**TABLE 2** Means and standard deviations (in parenthesis) of surface hardness (VHN) of the tested materials, before and after polishing at different times- I (immediately), 24h (24 hours), 7d (7 days), 21d (21 days)

| PERIOD  | MATERIAL          | Revolutio (n=40) | Natural Flow (n=40) | Flow-it! (n=40) | Fill Magic Flow (n=40) | Silux (n=40) | Z100 (n=40) |
|---------|-------------------|------------------|---------------------|----------------|------------------------|-------------|-------------|
|         |                   | I–before         | I–after             | 24h–before     | 24h–after              | 7d–before   | 7d–after    |
|         |                   | 20.05 d*         | 27.38 a*            | 24.75 a*       | 25.62 c*               | 27.93 a*    | 23.10 a*    |
|         |                   | (2.62) c*        | (2.52) a*           | (1.68) c*      | (1.65) c*              | (0.82) a*   | (2.21) a*   |
|         |                   | 20.60 (0.94) c*  | 29.93 (2.78) d*     | 21.97 a*       | 29.72 c*               | 28.61 (1.65) b* | 25.27 (1.82) a* |
|         |                   | 22.33 (2.78) c*  | 29.08 (2.88) d*     | 25.50 b*       | 31.23 c*               | 30.58 (1.80) b* | 32.03 (5.27) a* |
|         |                   | 28.95 (1.88) cd  | 30.43 (3.66) d*     | 33.95 (3.66) c* | 37.60 (1.35) b*        | 29.18 (8.67) d* | 43.62 (4.81) b* |
|         |                   | 35.03 (1.88) d*  | 35.92 (1.33) cd     | 33.48 (1.33) cd | 35.92 (2.03) d*        | 39.70 (2.30) b* | 41.33 (5.48) a* |
|         |                   | 99.47 (4.06) c*  | 96.53 (9.10) d*     | 94.40 (9.10) d* | 94.30 (4.76) d*        | 117.5 (10.36) a* | 140.8 (10.36) a* |
|         |                   | I–after           | 24h–before          | 24h–after      | 7d–before              | 7d–after    |
|         |                   | 25.62 b*          | 25.62 c*            | 25.62 c*       | 27.93 a*               | 23.10 a*    | 25.23 a*    |
|         |                   | (2.21) a*         | (1.65) c*           | (1.65) c*      | (0.82) a*              | (2.21) a*   | (1.52) c*   |
|         |                   | 29.72 (1.90) a*   | 31.23 (4.98) a*     | 29.72 (4.98) a* | 28.61 (1.65) a*        | 30.58 (1.80) a* | 32.03 (5.27) a* |
|         |                   | 37.60 (4.51) b*   | 38.70 (5.41) b*     | 30.58 (5.41) b* | 29.18 (1.80) b*        | 38.65 (8.67) d* | 43.62 (4.81) b* |
|         |                   | 38.00 (1.35) b*   | 38.00 (1.35) b*     | 38.00 (1.35) b* | 39.70 (1.35) b*        | 44.35 (2.30) b* | 41.33 (5.48) a* |
|         |                   | 117.5 (4.24) bc   | 117.5 (4.24) bc     | 117.5 (4.24) bc | 94.28 (4.24) bc        | 94.30 (2.70) b* | 94.30 (10.36) a* |
|         |                   |                  |                     |                |                        |             |             |

Same letters: statistical similarity - comparison in lines
Same symbol: statistical similarity - comparison in columns
Composite resins show microscopic alterations as a result of polymerization shrinkage, restoration technique and finishing/polishing procedures, which can lead to the formation of surface and sub-surface microdefects. If present in a significant amount, these structural microdefects can interfere with the material surface smoothness, wear resistance and hardness, thus significantly compromising its longevity and limiting its indication to some clinical situations.

The findings of this research disclosed that polishing influenced hardness of the tested composite resins, significantly increasing these values. These results were corroborated by another investigation, which also verified the influence of polishing using a minfilled composite resin. Although a smooth surface can be obtained after polymerization, the superficial layer is essentially composed by organic matrix, being hence, less dense than the underlying layer. Thus, the removal of this layer by polishing procedures increases the surface resistance.

Apart from hardness, polishing performed immediately after polymerization can also affect marginal integrity, leading to gaps formation at the tooth/restoration interface. This fact is also inherent to adhesive restorative materials, due to the stress generated by rotary instruments. Moreover, polishing can provide a more permanent deformation-resistant surface and, if polishing is accomplished immediately after polymerization, this incomplete maturation could turn composites more susceptible to the effects of heat generation, thereby decreasing their hardness, since approximately 75% of the light-curing process occurs in the first 10 minutes, and the curing reaction can continue for a period of up to 24 hours. Delayed polishing also allows the composite resin to become less liable to negative effects of heat created by this procedure.

Other finding observed in this study was the difference in the performance of tested materials. Flowable composites showed inferior results as compared to the microfilled and minfilled resins. For instance, Z100 minfilled composite resin is composed of zirconium-silica filler particles, which provide higher hardness than colloidal silica present in great amount in Silux Plus microfilled composite. Moreover, the amount of organic matrix present in Z100 is lesser than in the other tested resins.

In this work, the tested flowable composite resins presented similar performance and inferior results as compared to the microfilled and minfilled composite resins. However, irrespective of the composite, delayed polishing is recommended for obtaining better mechanical properties.

CONCLUSIONS

On the basis of these results, and within the limitations of an in vitro study, it may be concluded that:
1. Flowable composite resins showed lower hardness as compared to the microfilled and minfilled, regardless of polishing.
2. Polishing influenced superficial hardness of the composites, and delayed polishing after 7 days provided higher hardness values.
3. Z100 presented the highest hardness before and after polishing at the different evaluated intervals.

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