Albumin-assembled copper-bismuth bimetallic sulfide bioactive nanosphere as an amplifier of oxidative stress for enhanced radio-chemodynamic combination therapy

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Abstract

The tumor microenvironment with overexpressed hydrogen peroxide (H$_2$O$_2$) and reinforced antioxidative system (glutathione, GSH) becomes a double-edged sword for the accessibility of nano-therapy. Since reactive oxygen species (ROS) are easily quenched by the developed antioxidative network, ROS-based treatments such as chemodynamic therapy (CDT) and radiotherapy (RT) for killing cancer cells are severely attenuated. To overcome such limitations, a bioactive nanosphere system is developed to regulate intracellular oxidative stress for enhanced radio-chemodynamic combination therapy by using bovine serum albumin (BSA) based bioactive nanospheres that are BSA assembled with in situ generated copper-bismuth sulfide nanodots and diallyl trisulfide (DATS). The copper-bismuth sulfide nanodots react with H$_2$O$_2$ to produce •OH and release Cu$^{2+}$. Then, the Cu$^{2+}$ further depletes GSH to generate Cu$^+$ for more •OH generation in the way of Fenton-like reaction. Such a cascade reaction can initiate •OH generation and GSH consumption to realize CDT. The elevation of ROS triggered by the DATS from BBCD nanospheres further augments the breaking of redox balance for the increased oxidative stress in 4T1 cells. With the sensitization of increased oxidative stress and high Z element Bi, an enhanced radio-chemodynamic combination therapy is achieved. The current work provides an enhanced radio-chemodynamic combination treatment for the majority of solid tumors by using the co-assembled bioactive nanospheres as an amplifier of oxidative stress.

Keywords: bioactive materials; nanosphere; assembly; bismuth–copper; radio-chemodynamic therapy

Introduction

Intracellular redox status is maintained by dynamic equilibrium between reactive oxygen species (ROS) and the antioxidative defense system. ROS, such as hydroxyl radical (•OH), superoxide anion (O$_2^-$), singlet oxygen ($^1$O$_2$) and others, can cause cell death by oxidizing biological matter in cells [1–3]. The antioxidative system in cancer cells consists of multiple small molecules, antioxidant enzymes and other specific components [4–6]. As a ROS capturer, glutathione (GSH) is an important member in the antioxidative system that can neutralize ROS to protect cells from oxidative damage [7, 8]. The majority of solid tumors have a unique microenvironment with overexpressed GSH (≈10 mM) [9] and H$_2$O$_2$ (10–50 μM) [10]. This featured tumor microenvironment is an obstacle but also an opportunity for tumor therapy. The inadequate ROS generated from H$_2$O$_2$ in most solid tumor cells is still difficult to meet the requirements of high therapeutic efficiency [11]. So, a variety of emerging materials have been designed for the enhanced level of H$_2$O$_2$ or ROS in cancer cells [12–18]. For example, Koo et al. [19] synthesized the copper–iron peroxide nanoparticles for the supply of H$_2$O$_2$, and the Cu and Fe ions synergistically initiated the production of abundant ROS by the Fenton reaction. However, the reinforced antioxidative system in
tumor cells can eliminate ROS before their interaction with intracellular components to attenuate the outcome of ROS therapy [20]. So, a single nanosystem with enhanced ROS generation as well as GSH depletion is urgently needed for cancer therapy.

Radiotherapy (RT) is one of the most widely used treatments in clinic [21]. Great effort has been dedicated to meliorating the efficiency of RT [22, 23], for instance, high Z elements for X-ray deposition [24–26] and delivering oxygen for reversing hypoxia [27, 28]. However, the abnormal metabolism in tumor tissues triggers the mutation of redox homeostasis [29]. Oxidative damages (DNA double-strand destruction or lipid peroxidation) initiated by ionizing radiation (e.g. X-ray) are more easily repaired by the reinforced antioxidant system in cancer cells, resulting in a restricted RT [30, 31]. Therefore, disrupting the intra-tumoral redox balance for enhanced oxidative damage caused by ionizing radiation is a promising way of sensitization for RT.

Based on the predicament mentioned above, BSA-based copper-bismuth sulfide/DATS nanospheres (BBCD) are designed to modulate redox balance, constructing an internal microenvironment with a high level of oxidative stress in the tumor for amplified radio-chemodynamic combination therapy. As depicted in Fig. 1a, an integrated nanoplatform of BBCD is fabricated facilely through an in situ assembly route at room temperature. Bi³⁺ and Cu²⁺ chelated bovine serum albumin (BSA) assembles with diallyl trisulfide (DATS), thioacetamide (TAA) acts as the donor of S²⁻ to induce ultrasmall copper-bismuth sulfide (BC) nanodots growing inside organic molecules, BBCD nanospheres are obtained after aging. Nanospheres of BBC (BC nanodots loaded in BSA nanosphere) or BB (bismuth sulfide nanodots loaded in BSA nanosphere) are synthesized as control samples. The enhanced therapeutic efficacy by BBCD is illustrated in Fig. 1b. (i) Consumption of GSH for enhanced chemodynamic therapy (CDT). BBCD nanospheres interact with intratumoral GSH and H₂O₂ to generate ⋅OH and deplete GSH in the way of Fenton-like reaction. The GSH depletion leads to enhanced CDT. (ii) Increased oxidative stress. DATS can induce an enhanced level of ROS in 4T1 cells, and the elevated ROS and decreased GSH lead to amplified oxidative stress. (iii) Enhanced RT. The amplification of oxidative stress within tumor cells reverses the resistance induced by the antioxidative system, making 4T1 cells more sensitive to oxidative damage induced by RT. Thus, an amplified RT is achieved. In a word, BBCD nanospheres are successfully fabricated to prove an effective regulation of oxidative stress in 4T1 cells for elevated radio-chemodynamic combination therapy, providing a potential strategy for the sensitization of ROS-based tumor therapy.

**Materials and methods**

**Materials.** Bismuth nitrate pentahydrate (Bi(NO₃)₃·5H₂O, 99%), copper nitrate trihydrate (Cu(NO₃)₂·3H₂O, 99%), TAA, dimethyl sulfoxide (DMSO), nitric acid (HNO₃), melamine blue (MB, ≥82%) were purchased from Sinopharm Chemical Reagent Co., Ltd (China). DATS (≥98%) was bought from Beijing Jin Ming Biotechnology Co. Ltd. BSA, GSH, 3,3′,5,5′-tetramethylbenzidine (TMB), terephthalic acid (TPA) and 5,5′-dithiobis-(2-nitrobenzoic acid) (DTNB) were obtained from Sigma-Aldrich. No further purification for all used reagents were operated. The catalog numbers of reagents: Bi(NO₃)₃·5H₂O (Sinopharm Chemical Reagent Co., Ltd, catalog number: 80018318), Cu(NO₃)₂·3H₂O (Sinopharm Chemical Reagent Co., Ltd, catalog number: 10007916), TAA (Sinopharm Chemical Reagent Co., Ltd, catalog number: 30177714), DMSO (Sinopharm Chemical Reagent Co., Ltd, catalog number: 30072428), DATS (Beijing Jin Ming Biotechnology Co., Ltd, catalog number: D60006), nitric acid (Sinopharm Chemical Reagent Co., Ltd, catalog number: 10014528), BSA (Sigma-Aldrich, B265993-25g), MB (Sinopharm Chemical Reagent Co., Ltd, catalog numbers: 71024544), GSH (Sigma-Aldrich, D15427-5g), 3,3′,5,5′-tetramethylbenzidine (Sigma-Aldrich, T100417), TPA (Sigma-Aldrich, P108506-100g), 5,5′-dithiobis-(2-nitrobenzoic acid) (Sigma-Aldrich, D105559).

**Synthesis and characterization**

**Synthesis of BBCD**

BBCD nanospheres were synthesized through a modified method based on the previous report [32]. Forty-eight milligrams of Bi(NO₃)₃·5H₂O were dissolved in 2 ml HNO₃ (1.5 M) solution, 12 mg Cu(NO₃)₂·3H₂O were dissolved in 2 ml deionized H₂O and 15 mg BSA were dissolved in 20 ml deionized water. Then, the solution of Bi³⁺ and Cu²⁺ were dropwise added into BSA solution, respectively. After 30 min stirring, 20 mg DATS in 200 μl DMSO were injected into above mixture. Thirty minutes later, 2 ml TAA solution (0.004 g/ml) was added slowly for another 6 h stirring at 25°C. Then, BBCD nanospheres were obtained by centrifugation at 12 000 rpm for 10 min. BBCD nanospheres were synthesized in the same procedure described above without the addition of DATS. BB nanospheres were synthesized in the same route described above without addition of Cu(NO₃)₂·3H₂O and DATS.

**Characterization**

Transmission electron microscopy (TEM) images and high-resolution TEM (HRTEM) images were captured by Talos F200X electron microscope. Scanning electron microscopy (SEM) images were taken by Nova NanoSEM 450 electron microscope. Energy dispersive spectrometry (EDS) mapping (Talos F200X) and X-ray fluorescence (XRF) (EAGLE III) were used to analyze the composition of elements in nanospheres. The X-ray diffraction (XRD) analysis of samples were operated on X’Pert3 Powder. X-ray photoelectron spectroscopy (XPS) analysis for the valence state of...
elements in samples were conducted on machine of AXIS-ULTRA DLD-600W. Inductively coupled plasma-mass spectrometry (ICP-MS) analysis for the content of elements in samples was operated on PerkinElmer ELAN DRC-e. The level of DATS in BBCD was determined by thermogravimetric (TG) analyzer (Diamond TG/DTA, PerkinElmer), with an increasing rate of 20°C/min from room temperature to 650°C under air atmosphere. Fourier transform infrared spectroscopy (FT-IR) and UV–vis absorption of the samples were recorded through Nicolet iS50R (Thermo Scientific) and SolidSpec-3700 (Shimadzu) spectrophotometer. FP-6500 (Jasco) spectrometer was used to detect the fluorescence spectra. Fluorescence microscope (Nikon Ti2-U) and flow cytometer were used for the fluorometric analysis.

**Reaction of BBCD with H$_2$O$_2$ or GSH**

**Reaction between BBCD and H$_2$O$_2$**

BBCD (100 μg/ml) reacted with H$_2$O$_2$ (10 mM) in PBS solution at 37°C for 12 h. The precipitations obtained by centrifugation at different times (30 min, 1, 2 and 12 h) were characterized by TEM. After 12 h reaction, the precipitates (BBCD$_{12}$) were collected for the analysis of XPS, XRD and XRF.

- •OH production from Cu$^{2+}$ reacted with H$_2$O$_2$, TMB (50 μg/ml) and Cu$^{2+}$ (1 mM) and H$_2$O$_2$ (1 mM or 10 mM) in PBS solution at 37°C. BBCD (100 μg/ml) reacted with H$_2$O$_2$ (10 mM) in a PBS solution containing TMB (50 μg/ml) at 37°C. The system of TMB, TMB + Cu$^{2+}$, TMB + H$_2$O$_2$ were set as the control groups. After 2 h reaction, all systems were centrifuged at 10,000 rpm for the detection of absorption at 650 nm via UV–vis spectroscopy.

**Degradation of MB and TPA oxidation**

MB (20 μg/ml) and (i) BBCD (100 μg/ml), (ii) BBC (88 μg/ml) and (iii) BB (91 μg/ml) were treated with H$_2$O$_2$ (10 mM) in PBS solution, the degradation of MB induced by •OH at different time were measured through UV–vis spectroscopy. The persistently generation of •OH was measured via TPA oxidation at various concentrations of H$_2$O$_2$. PBS solutions including TPA (1 μg/ml), BBCD (100 μg/ml) and different concentration of H$_2$O$_2$ (0, 0.5, 1, 5 and 10 mM) were stirred at 37°C for 2 h, then the fluorescence intensity induced by excitation wavelength at 315 nm was measured at around 430 nm.

**Reaction of BBCD with GSH**

BBCD (1 mg/ml) reacted with GSH (1 mM) in PBS solution at 37°C for 12 h. Then, the precipitates (BBCD$_{12}$) were obtained by centrifugation for the XPS analysis.

**Depletion of GSH in solution**

The reaction between GSH and DTNB was used to measure the GSH depletion in solution. GSH (1 mM), H$_2$O$_2$ (0 μM or 500 μM) and (i) no additive as control, (ii) BB (0.91 μg/ml), (iii) BBC (88 μg/ml) or (iv) BBCD (1 mg/ml) in PBS were stirred at 37°C for 2 h, and then centrifuged (10,000 rpm) to remove precipitates. The supernatant was incubated with DTNB solution (5 mg/ml, 10 μl) in 96-well plates (n = 3) for measurement of absorbance at 412 nm on a microplate reader (Biotech ELx808, USA).

**Cell culture**

The 4T1 cancer cells were purchased from Wuhan Kehaojia Biotechnology Co., LTD. Mouse bone marrow stromal cells (BMSC) and human umbilical vein vessel endothelial cells (HUVECs) were obtained from Advanced Biomaterials and Tissue Engineering Center, HUST. All the cells were cultured with DMEM (including 10% fetal bovine serum) in a humidified 5% CO$_2$ incubator at 37°C.

**Analysis of intracellular ROS and GSH/GSSG**

**Evaluation of intracellular ROS**

4T1 cells were seeded into 6-well plates with a density of 1 × 10$^6$ cells per well. After 12 h incubation, the culture medium was replaced with fresh medium, which included: (i) no additive as control, (ii) BB (91 μg/ml), (iii) BBC (88 μg/ml), (iv) BBCD (100 μg/ml). After 18 h co-culturing, the treated cells were washed by PBS and incubated with 2’,7’-dichlorodihydrofluorescein diacetate (DCFH-DA, 10 μM in pure DMEM) for 30 min at 37°C in dark. The stained cells were analyzed by fluorescence microscope and flow cytometer.

4T1 cells were pretreated by BB (91 μg/ml), BBC (88 μg/ml) or BBCD (100 μg/ml) for 12 h, then exposed to X-ray irradiation (6 Gy). After another 6 h culturing, the treated cells were washed by PBS and stained by DCFH-DA (10 μM). ROS in treated cells were tested by fluorescence microscope and flow cytometer.

4T1 cells were pretreated by BB (91 μg/ml) + GSH (500 μM), BBC (88 μg/ml) + GSH (500 μM) or BBCD (100 μg/ml) + GSH (500 μM) for 12 h, then exposed to X-ray irradiation (6 Gy). The ROS level in treated cells were tested by fluorescence microscope after another 6 h incubation.

**Detection of intracellular GSH**

The GSH/GSSG assay kit (Beyotime, Jiangsu, China) was used to detect intracellular GSH and GSSG. 4T1 cells were cultured in six-well microplates (1 × 10$^6$ cells per well) for 12 h. Then the medium was replaced by fresh medium, which contained: (i) no additive as control, (ii) BB (91 μg/ml), (iii) BBC (88 μg/ml), (iv) BBCD (100 μg/ml). After 12 h incubation, the treated cells were washed by PBS and collected. Solution of protein removal reagent was mixed with the treated cells for rapid vortex, and then the samples were subjected to two rapid freeze–thaw cycles in liquid nitrogen and 37°C water bath. The supernatant was obtained after centrifugation of 10,000 g for 10 min. Detection of GSH and GSSG in samples was performed according to the protocol in GSH/GSSG assay kit.

**Western blotting assay and RNA-sequencing**

4T1 cells were treated in the same way as the experiment of GSH detection. The treated cells were mixed with appropriate amount of RIPA lysate containing 1 mmol/L phenylmethylsulfonyl fluoride and phosphatase inhibitors (Servicebio, Wuhan) for 30 min incubation. The samples were centrifuged (12,000 rpm, 30 min at 4°C) to collect the supernatant. The protein samples were subjected to 10% polyacrylamide SDS-PAGE. Then the primary antibodies anti-HMOX1 (1:1000, Abclonal, A19162) and anti-GAPDH (1:4000, Abclonal, AC002) were used for the analysis of immunoblots. After incubation with the goat anti-rabbit IgG secondary antibody, signals of protein were recorded.

4T1 cells were seeded in 6-well plates with a density of 1 × 10$^6$ cells per well for 24 h incubation. The 4T1 cells incubated with BBCD (100 μg/ml) for 12 h. Then the treated 4T1 cells were collected to perform the high-throughput sequencing (Wuhan SeqHealth Tech Co., Ltd).

**Tumor killing in vitro**

**Cytotoxicity in vitro**

The cell viability was measured by CCK-8 (Cell Counting Kit-8, US EVERSIGHT INC). 4T1 cells were seeded in 96-well microplates (6 × 10$^3$ cells per well) for 24 h incubation. The 4T1 cells were
treated with BB, BBC or BBCD at different concentration. After another 36 h incubation, the cell viability was detected by microplate reader. 4T1 cells were pretreated by different concentration of BBCD (BB, BBC) for 12 h, then exposed to X-ray irradiation (6 Gy). After another 24 h incubation, the viability of 4T1 cells was tested.

**Calcein-AM and PI staining**

$1 \times 10^6$ 4T1 cells per well were cultured in six-well plates at 37°C for 24 h. Then the 4T1 cells were treated in the same way as the experiment of cytotoxicity in vitro. The groups were named as: (i) no treating as control, (ii) BB (91 μg/ml), (iii) BBC (88 μg/ml), (iv) BBCD (100 μg/ml), (v) RT, (vi) BB (91 μg/ml) + RT, (vii) BBC (88 μg/ml) + RT, (viii) BBCD (100 μg/ml) + RT. Finally, the treated 4T1 cells were washed with PBS and stained by Calcein-AM (10 μM) and PI (20 μM) (US EVERBRIGHT INC.).

**Detection of DNA damage in treated 4T1 cells**

γ-H2AX immunofluorescent staining were used to detect the breakage of DNA double-strand in treated 4T1 cells. 4T1 cells in six-well plates were co-cultured with BB (91 μg/ml), BBC (88 μg/ml) or BBCD (100 μg/ml) for 12 h, then exposed to X-ray irradiation (0 or 2 Gy). After 24 h incubation, all groups were washed with PBS for staining of γ-H2AX immunofluorescent. The images of immunofluorescence were obtained through fluorescence microscope.

**Tumor therapy in vivo**

**Animals**

Balb/c mice were obtained from the Laboratory Animal Center, Three Gorges University (Yichang, China). The animal experiments were approved by the Animal Experiment Ethics Committee of Huazhong University of Science and Technology.

**Tumor models**

Balb/c mice (female, 6 weeks) were subcutaneously injected with 100 μl PBS containing $\approx 10^6$ 4T1 cells. When the tumor volume reached $\approx 60 \text{ mm}^3$, the Balb/c mice were randomly divided into eight groups (n = 3): (i) PBS, (ii) BB, (iii) BBC, (iv) BBCD, (v) PBS + RT, (vi) BB + RT, (vii) BBC + RT, (viii) BBCD + RT. All mice received tail intravenous injection, and the injection dosage was based on the Bi content ($[\text{Bi}] = 10 \text{ mg/kg}$). Eighteen hours after injection, the pretreated mice were exposed to X-ray irradiation (0 or 6 Gy). The same treatments were performed at Day 1, 4 and 7. During the period of 21 days treatment, the tumor volume and body weight of all mice were recorded every 3 days. The tumor volume was calculated by the equation of $V = \frac{1}{2}(L \times W)^2$, the letter L, W and V were representative of the length, width and volume of tumor, respectively. At Day 22, the tumors of all mice were stripped for the length, width and volume of tumor, respectively. The results of XRD analysis for BBC, BBC and BB were shown in Fig. 2a. The two broad peaks in XRD pattern of BB were indexed to the standard card of Bi$_2$S$_3$ (JCPDS Card No. 0-0320). Combining the HRTEM and XRD results of BB (Supplementary Fig. S3b), it was concluded that nanodots in BB were bismuth sulfide with poor crystallinity or non-crystallinity [33]. With the addition of Cu, the first diffraction peak in the XRD pattern of BBCD or BBC shifted to a higher diffraction angle, indicating the doping of Cu in bismuth sulfide [34]. XPS analysis was performed to elucidate the valence state of elements in the BBCD nanosphere (Supplementary Fig. S4).

**Results and discussion**

**Synthesis and characterization of BBCD**

From the images of TEM and SEM (Fig. 2a; Supplementary Fig. S1a–d), monodisperse BBCD spheres with relatively uniform size were obtained. There were about 5 nm nanodots embedded in the organic matrix (Fig. 2b), and no lattice fringes were found by the characterization of HRTEM (Fig. 2c). The images of EDS elemental mapping depicted the elements distribution in the BBCD nanosphere (Fig. 2d and e). As expected, bismuth (Bi), copper (Cu), sulfur (S), nitrogen (N) and trace oxygen (O) elements were throughout the entire spheres with an even distribution. The BBCD spheres have an average size of 80 nm and a larger average hydrodynamic size of 115 nm in PBS (Fig. 2f; Supplementary Fig. S1e). BBC and BB shared the similar characteristics with BBCD (Supplementary Fig. S2 and S3a).

The results of XRD analysis for BBC, BBC and BB were shown in Fig. 2g. The two broad peaks in XRD pattern of BB were indexed to the standard card of Bi$_2$S$_3$ (JCPDS Card No. 17-0320). Combining the HRTEM and XRD results of BB (Supplementary Fig. S3b), it was concluded that nanodots in BB were bismuth sulfide with poor crystallinity or non-crystallinity [33]. The asymmetric peaks of Bi 4f in the BBCD nanosphere were deconvoluted into four peaks (Fig. 2i). The binding energies at 932.3 and 952.2 eV were assigned to Cu 2p$_{3/2}$ and Cu 2p$_{1/2}$ (Fig. 2h), which corresponded to the standard values of Cu$_{4+}$ in Cu–S bond [35]. There was no difference between the binding energies of Cu 2p in BBCD and BBC (Supplementary Fig. S5).

**Toxicity of BBCD to normal cells and tissues**

**Toxicity in vitro**

CCK-8 assay for cell viability of BMSC and HUVECs in vitro were performed to detect the acute cytotoxicity induced by BBCD. BMSC or HUVECs were seeded in 96-well microplates. When the cells density reached 80% of the well area, the cells treated with different concentration of BBCD for 24 h. Then, the cell viability was determined according to the absorbance at 450 nm on microplate reader.

**Toxicity in vivo**

Biochemical analysis of blood and histological analysis of major organs were performed to evaluate the long-term toxicity of BBCD in vivo. Healthy Balb/c mice (female, 6 weeks) were randomly divided into 3 groups (n = 3). (i) Control (healthy mice), (ii) 1 day (1 day after tail intravenous injection of BBCD [Bi] = 10 mg/kg), (iii) 21 days (21 days after tail intravenous injection of BBCD [Bi] = 10 mg/kg). The fresh blood from all mice were extracted for biochemistry analysis, and the major organs (heart, liver, spleen, lung and kidney) were collected for the staining of H&E.

**Statistical analysis**

All data were expressed in the way of mean ± standard deviation (SD). The analysis of statistical difference was operated through one-way analysis of variance (ANOVA).

**ICP-MS analysis of BBCD or BBC**

In Table 1, the molar ratio of Bi and Cu in BBCD was not distinctly different from the molar ratio of Bi and Cu in BBC. Based on the ICP-MS analysis of BBCD or BBC and the results of XRD analysis for BBC, BBC and BB, it was found that nanodots in BB were bismuth sulfide with poor crystallinity or non-crystallinity [33]. The asymmetric peaks of Bi 4f in the BBCD nanosphere were deconvoluted into four peaks (Fig. 2i). The binding energies at 932.3 and 952.2 eV were assigned to Cu 2p$_{3/2}$ and Cu 2p$_{1/2}$ (Fig. 2h), which corresponded to the standard values of Cu$_{4+}$ in Cu–S bond [35]. There was no difference between the binding energies of Cu 2p in BBCD and BBC (Supplementary Fig. S5). The asymmetric peaks of Bi 4f in the BBCD nanosphere were deconvoluted into four peaks (Fig. 2i). The binding energies at 932.3 and 952.2 eV were assigned to Cu 2p$_{3/2}$ and Cu 2p$_{1/2}$ (Fig. 2h), which corresponded to the standard values of Cu$_{4+}$ in Cu–S bond [35]. There was no difference between the binding energies of Cu 2p in BBCD and BBC (Supplementary Fig. S5).
between the molar ratio of Bi:Cu (BBCD) and Bi:Cu (BBC), n = 3. The FT-IR spectra of BBCD, BBC and DATS were presented in Fig. 2j. The characteristic peaks at 985 and 919 cm⁻¹ belonged to the –CH and =CH₂ groups in DATS [40, 41], which were only found in the FT-IR spectra of BBCD or DATS, suggesting the successful loading of DATS in BBCD. There were 8 wt.% DATS in BBCD, 61 wt.% copper-bismuth sulfide in BBCD, 69 wt.% copper-bismuth sulfide in BBC and 60 wt.% bismuth sulfide in BB, respectively (Fig. 2k; Supplementary Fig. S7).

Mechanism of ⋅OH generation and GSH elimination
Based on the findings of TG and ICP-MS analysis, the concentrations of BBCD, BBC and DATS were presented in Fig. 2. The characteristic peaks at 985 and 919 cm⁻¹ belonged to the –CH= and =CH₂ groups in DATS [40, 41], which were only found in the FT-IR spectra of BBCD or DATS, suggesting the successful loading of DATS in BBCD. There were 8 wt.% DATS in BBCD, 61 wt.% copper-bismuth sulfide in BBCD, 69 wt.% copper-bismuth sulfide in BBC and 60 wt.% bismuth sulfide in BB, respectively (Fig. 2k; Supplementary Fig. S7).

Firstly, the generated ⋅OH from reaction between Cu²⁺ and H₂O₂ was confirmed by the elevated intensity of absorption at around 650 nm (Supplementary Fig. S8). Next, the ⋅OH generation from BBCD reacting with H₂O₂ was demonstrated by the oxidation of TMB. Addition of BBCD into the solution including TMB and H₂O₂ contributed to an obvious absorption peak, which proved that BBCD catalyzed H₂O₂ decomposing into ⋅OH (Supplementary Fig. S9). The degradation of MB in the reaction system containing BBCD and H₂O₂ within a prolonged time was used to explore the continuous production of ⋅OH [9]. As presented in Fig. 3a, the gradually decreasing absorption peaks at ~660 nm were indicative of BBCD interacting with H₂O₂ to produce ⋅OH persistently. A significantly enhanced fluorescence intensity was probed at around 430 nm from the oxidation system of TPA with an increasing level of H₂O₂, which indicated that the increased concentration of H₂O₂ was helpful to ⋅OH generation (Fig. 3b) [9]. BBC had the same ability to react with H₂O₂ to produce ⋅OH as BBCD (Supplementary Fig. S10a). On the contrary, no detectable ⋅OH was observed from the system of BB incubating with H₂O₂ (Supplementary Fig. S10b). These phenomena revealed that the Cu²⁺ species in BBCD or BBC drove the generation of ⋅OH from H₂O₂.
To investigate the reaction process between BBCD and H₂O₂, BBCD was incubated with H₂O₂ at 37°C for 12 h. The precipitates obtained from centrifugation were labeled as BBCDH. It was interesting to find that BBCD nanosphere was losing morphology during incubation of H₂O₂, and new crystals grew in the BBCDH (Supplementary Fig. S11). The elements in BBCDH were explored by EDS elemental mapping and XRF analysis. There was no Cu element in BBCDH (Supplementary Figs S12 and S13). The XRD pattern of BBCDH displayed the diffraction peaks assigned to a mixture of bismuth oxide sulfate, which were the new grown crystals in BBCDH (Supplementary Fig. S14). BBCDH was further investigated by XPS analysis (Fig. 3c and d). There were no peaks found in the high-resolution XPS spectra of Cu 2p in BBCDH, indicating that there was no Cu in BBCDH, which was consistent with the element analysis of BBCDH. The peaks of Bi 4f (Bi–S) and S 2p disappeared in the high-resolution XPS spectra of BBCDH. The peaks at 159.3 and 164.6 eV were assigned to Bi 4f 7/2 and Bi 4f 5/2, respectively, which were 0.5 eV lower than the Bi 4f in BBCD-G (mean ± SD, non-significance was expressed as n.s., and "P < 0.05, "**P < 0.01, "***P < 0.001, n = 3).

Then, 5,5'-dithiobis-(2-nitrobenzoic acid) (DTNB) was used as a director to assess the GSH depletion by BBCD. The products from DTNB reacting with GSH displayed a characteristic absorption peak at around 412 nm [45]. As shown in Fig. 3e, BBCD or BBC induced the depletion of GSH directly, while BB could not apparently deplete GSH. And compared with the control group, with the addition of H₂O₂, there was a 54% decrease of GSH in the group of BBCD, a 46% reduction of GSH in the group of BBC, and only a 9.9% loss of GSH in the group of BB (Fig. 3f). A significant elimination of GSH by BBCD or BBC was realized with the assistance of H₂O₂. BB had a weak ability to deplete GSH with the assistance of H₂O₂, which could be ascribed to the disassembly of BB by H₂O₂.

**Amplified oxidative stress by BBCD for enhanced radio-CDT in vitro**

The physical and chemical properties of BBCD had been evaluated in detail. BBCD showed excellent reactivity with H₂O₂ or GSH in solution. The performance of BBCD in vitro was explored to assess the therapeutic outcome of combination therapy for 4T1 cancer cells.

ROS generation and GSH depletion in vitro were tested to discuss the interaction between 4T1 cells and BBCD. Intracellular ROS was assessed by the probe of 2’,7’-dichlorodihydrofluorescein diacetate (DCFH-DA), which could be oxidized into DCF with green fluorescence and a stronger fluorescence implying more ROS. Figure 4a shows the ROS levels in treated 4T1 cells. Compared with the BB or untreated group, BBCD or BBC treatment led to a higher level of ROS. BBCD or BBC reacted with

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**Figure 3.** (a) UV–vis absorption spectra for the degradation of MB, which was incubated with BBCD and H₂O₂. \([\text{BBCD}]=100 \mu\text{g/ml}, [\text{H}_2\text{O}_2]=10 \text{mM}, [\text{MB}]=20 \mu\text{g/ml}.\) (b) Fluorescence spectra of TPA oxidized by •OH generated from H₂O₂ reacting with BBCD. \([\text{BBCD}]=100 \mu\text{g/ml}, [\text{TPA}]=1 \text{mg/ml} .\) (c, d) High-resolution XPS spectra of Cu 2p, Bi 4f and S 2p in BBCDG (mean ± SD). (e) GSH depleted by BBCD, BBC and BB. GSH as the control group. \([\text{BBCD}]=1 \text{mg/ml}, [\text{GSH}]=1 \text{mM}.\) (f) GSH depleted by BBCD, BBC or BB with addition of H₂O₂. The control group was GSH + H₂O₂ \([\text{BBCD}]=1 \text{mg/ml}, [\text{GSH}]=1 \text{mM}, [\text{H}_2\text{O}_2]=500 \mu\text{M}.\) (g, h) High-resolution XPS spectra of Cu 2p, Bi 4f and S 2p in BBCDH (mean ± SD, non-significance was expressed as n.s., and "P < 0.05, "**P < 0.01, "***P < 0.001, n = 3).
**Figure 4.**

(a, b) Representative fluorescence images and flow cytometry measurement of ROS in 4T1 cells. The untreated cells as control, [BB] = 91 μg/ml, [BBC] = 88 μg/ml, [BBCD] = 100 μg/ml. (c, d) Relative GSH and GSSG content in 4T1 cells. The untreated cells as control, [BB] = 91 μg/ml, [BBC] = 88 μg/ml, [BBCD] = 100 μg/ml. (e) Western blotting analysis for the expression of HMOX1 in 4T1 cells. The untreated cells as control, [BB] = 91 μg/ml, [BBC] = 88 μg/ml, [BBCD] = 100 μg/ml. RNA-seq for 4T1 cells (control) and BBCD treated 4T1 cells (BBCD). [BBCD] = 100 μg/ml. Differential expression of genes between the control and BBCD groups (f). Heatmap for the differential genes related to metal homeostasis and response to oxidative stress in treated 4T1 cells (g). GO enrichment analysis for the BBCD treated 4T1 cells (h). (i, j) Representative fluorescence images and flow cytometry detection of ROS in 4T1 cells. [BB] = 91 μg/ml, [BBC] = 88 μg/ml, [BBCD] = 100 μg/ml, X-ray irradiation (RT): 6 Gy. (k) The cytotoxicity of BB, BBC or BBCD to 4T1 cells. (l) The cancer killing induced by radio-chemodynamic combination therapy. RT (6 Gy) treatment alone as the control group. (m) Enhanced therapeutic efficacy in vitro (mean ± SD, non-significance was expressed as n.s., and *P < 0.05, **P < 0.01, ***P < 0.001, n = 3).
in intracellular GSH and H$_2$O$_2$, leading to GSH elimination and •OH production. Furthermore, it was found that DATS treatment could effectively elevate the ROS level in 4T1 cells (Supplementary Fig. S15). This was another important factor for BBCD owning the stronger ability to improve the intracellular ROS level compared with BBC or BB. The ROS concentration in treated 4T1 cells was reconfirmed by measurement of flow cytometry (Fig. 4b), and the variability trends of ROS level were consistent with the result of staining.

Meanwhile, the levels of GSH and GSSG in treated 4T1 cells were determined by the GSH and GSSG assay kit. As demonstrated above, BBCD and BBC exhibited a similar capacity for the elimination of GSH in solution because of the same component. The excess generation of ROS led to more GSH being eliminated [48]. Compared with the result of staining.

Intracellular ROS and GSH played critical roles in redox homeostasis, changes in ROS or GSH levels resulted in redox imbalance and increased oxidative stress [49]. The up-regulated expression of HMOX1 was regarded as a marker of amplified oxidative stress induced by a break in redox balance [50–53]. The western blotting (WB) assay was performed to identify the level of oxidative stress in treated 4T1 cells (Fig. 4e). Compared with the BB or control (untreated) group, the expression of HMOX1 in 4T1 cells treated by BBC or BBCD was apparently up-regulated. Further, HMOX1 in the BBCD treated group was more significantly up-regulated than it was in the BBC group, which was due to the more powerful regulation of ROS and GSH by BBCD in 4T1 cells. The increased oxidative stress achieved by BBCD was confirmed by mRNA-sequencing for the 4T1 cells treated by BBCD. In detail, a total of 14141 genes were detected, with 620 up-regulated genes and 817 down-regulated genes (Fig 4f). As shown in Fig 4g, a large number of genes related to metal homeostasis and oxidative stress response were observed by GO analysis of the differential genes with log2 FC > 1.5, which demonstrated that the BBCD successfully entered the cell and activated the signaling pathway of metal ion metabolism. The differentially expressed genes in theBBCD treated 4T1 cells were mostly associated with oxidative stress-related pathways like autophagy, heme catabolic process, and oxidoreductase activity (Fig. 4h).

Taken together, BBCD treatment could increase the oxidative stress of 4T1 cells.

The high level of antioxidative substances in cancer cells was a significant factor for the attenuation of ROS. The decreased GSH and increased ROS for elevated oxidative stress in tumor cells were beneficial for the ROS based therapy [54, 55]. Then, BBCD initiating the elevation of oxidative stress for enhanced radio-CDT was explored in vitro. 4T1 cells were pretreated with BB, BBC or BBCD, and then exposed to X-ray irradiation. The intracellular ROS level in treated groups (BB + RT, BBC + RT and BBCD + RT) were detected (Fig. 4i and j). Relative to the group of RT alone, the ROS in the group of BB + RT, BBC + RT or BBCD + RT were apparently elevated, and the maximum level of ROS in the BBCD + RT group was observed. This enhancement of ROS could be attributed to the radiosensitization induced by increased oxidative stress and the high Z element of Bi. GSH was used to investigate the effects of antioxidative substances on ROS production. 4T1 cells were pretreated with GSH + BBCD, then exposed to X-ray irradiation. As displayed in Supplementary Fig. S16, the ROS level in all groups induced by RT was significantly attenuated with the pretreatment of GSH. It implied that increased oxidative stress was conducive to the generation of ROS.

Next, the cell counting kit-8 (CCK-8) assay was used for quantitative analysis of the treatment outcome in vitro. The cytotoxicity of BBCD, BBC or BB to 4T1 tumor cells were explored. After 36 h incubation with BBCD (100 μg/ml) or BBC (88 μg/ml), ~40% and 22% 4T1 cells were killed by BBCD and BBC, respectively, and BB (91 μg/ml) showed no obvious cytotoxicity to 4T1 cells (Fig. 4k).

Figure 5. (a) Typical images of Calcine-AM and PI staining. No treatment as the control group, [BB] = 91 μg/ml, [BBC] = 88 μg/ml and [BBCD] = 100 μg/ml for 12 h pretreatment, then exposed to X-ray irradiation (0 or 6 Gy) followed by another 24 h incubation. (b) Representative images of y-H2AX immunofluorescence for DNA double-strand damage. No treatment as the control group, [BB] = 91 μg/ml, [BBC] = 88 μg/ml, [BBCD] = 100 μg/ml for 12 h pretreatment, then exposed to X-ray irradiation (0 or 2 Gy) followed by another 24 h incubation.
killed in the group of BBCD (100 μg/ml) + RT, 48% and 12% 4T1 cells were killed in the groups of BBC (88 μg/ml) + RT and BB (91 μg/ml) + RT (Fig. 4l). As displayed in Fig. 4m, BB (91 μg/ml) + RT treatment led to an 8% decrease in cell viability compared with BB (91 μg/ml) treatment alone. There was a 26% reduction in cell viability induced by BBC (88 μg/ml) + RT than by BBC (88 μg/ml) and the cell viability of BBCD (100 μg/ml) + RT group was 45% lower than the BBCD (100 μg/ml) group. The 8% decrease in cell viability between the groups of BB and BB + RT was ascribed to the high Z element of Bi for radiosensitization. The elevated 26% and 45% death of 4T1 cells were assigned to the enhancement of combination therapy induced by increased oxidative stress and high Z element of Bi (Supplementary Fig. S17). Compared with the 8% enhancement in cell killing induced by the high Z element of Bi, BBCD for radio-chemodynamic treatment of 4T1 cells induced a 45% elevation in cell killing to indicate that increased oxidative stress was the main factor for augmented combination therapy.

The killing efficiency of 4T1 cells by different treatments were reconfirmed by the live/dead cell staining assay. After different treatments, 4T1 cells were co-stained by calcein-AM and propidium iodide. BBCD combined with RT to kill the most 4T1 cells (Fig. 5a). The damage of DNA double-strand induced by treatments were explored through the staining of γ-H2AX immunofluorescence. A brightest red (DNA double-strand breaking) in the 4T1 cells of BBCD + RT group was detected, which implied that BBCD could effectively augment the damage of radiation to DNA (Fig. 5b). Based on the above investigations at the cellular level,

Figure 6. (a) Procedure of radio-chemodynamic combination therapy for the 4T1 tumor-bearing balb/c mice. (b) A photograph of the dissected tumors from treated mice. (c) The volume of tumors during the period of therapy. (d) The weight of dissected tumors from mice. (e) The body weight of tumor-bearing mice during therapy. (f) H&E, TUNEL and γ-H2AX immunofluorescence staining results of tumor sections after 21 days of treatment (mean ± SD, non-significance was expressed as n.s., *P < 0.05, **P < 0.01, ***P < 0.001, n = 3).
an enhanced outcome of radio-chemodynamic combination therapy in vivo was achieved by BBCD through the effective regulation of oxidative stress.

**Enhanced radio-CDT induced by BBCD in vivo**

Based on the experiments in vitro, we explored the application of BBCD for radio-chemodynamic combination therapy in vivo through the model of subcutaneous 4T1 tumor-bearing Balb/c mice (female, 6 weeks). The mice were randomly divided into eight groups: (i) PBS; (ii) BB; 3 BBC; (iv) BBCD; (v) PBS + RT; (vi) BB + RT; (vii) BBC + RT; (viii) BBCD + RT. All the mice received intravenous injection first, and 18 h later, the mice were exposed to X-ray irradiation. The same treatments were performed on Day 1, 4 and 7 (Fig. 6a).

After 21 days of treatment, the tumor sizes in the group of BBCD + RT were apparently smaller than others (Fig. 6b). BBCD effectively suppressed the growth of tumor, and the BBCD + RT treatment showed the strongest ability to inhibit the growth of tumor in vivo. Compared with the treatment of BB or RT, the BB + RT treatment induced a 56% and a 24% decrease in tumor volume, respectively. However, the BBCD + RT treatment induced a 77% and a 74% decrease in tumor volume compared with the treatment of BBCD or RT (Fig. 6c). Furthermore, the tumors in the BBCD + RT treatment group were the lightest among all the groups (Fig. 6d). During the 21 days of treatment, the body weight of all groups showed no significant abnormality (Fig. 6e).

The histological assessment of therapeutic efficacy was performed by H&E staining, TUNEL staining and γ-H2AX immunofluorescence staining (Fig. 6f). In comparison to all other groups, the visible contraction of cell nucleus, increased apoptosis and DNA double-strand breaking were observed in the BBCD + RT group. These results demonstrated that BBCD enhanced radio-CDT for the 4T1 tumor in vivo by the increased oxidative stress and high Z element.

**Cell viability of BMSC and HUVECs**

The acute toxicity of BBCD nanospheres to normal cells was evaluated by the interaction of BBCD with BMSC or HUVECs in vitro. The cell viability of BMSC or HUVECs did not change obviously after 24 h of co-incubation with BBCD, indicating that BBCD nanospheres had no cytotoxicity to normal cells (Supplementary Fig. S18).

**Histological observation and blood biochemical analysis**

Then, the long-term toxicity of BBCD nanospheres to normal tissues in vivo was investigated through the histological analysis of the main organ as well as biochemical analysis of the blood from the BBCD injected healthy mice. After 1 day or 21 days of injection, fresh blood from the injected mice was collected for the biochemical analysis of alanine aminotransferase (ALT), aspartate aminotransferase (AST), UREA and creatinine (CREA). Compared with healthy Balb/c mice (control), the ALT and AST data of liver function for injected mice (1 and 21 days) showed no abnormality, as did the UREA and CREA indexes of kidney function (Fig. 7a–d). Compared with the healthy mice (control), no obvious damage to major organs was observed from the results of H&E staining (Fig. 7e). As demonstrated by the investigations in vitro and in vivo, BBCD nanospheres were safe for the application of tumor therapy.

**Conclusion**

In summary, BBCD bioactive nanospheres were successfully constructed through an in situ assembly approach by BSA, copper-bismuth sulfide nanodots and DATS. It was demonstrated that those in situ grown copper-bismuth sulfide nanodots in the BBCD nanosphere could interact with the overexpressed H2O2 and GSH in 4T1 cells to achieve CDT via •OH generation and GSH elimination. At the same time, the DTAS from BBCD nanospheres could further induce the elevation of ROS in 4T1 cells. The efficient modulation of ROS and GSH by BBCD resulted in the breaking of antioxidant system for a significant up-regulation of intracellular oxidative stress, which enhanced the sensitivity of 4T1 tumor cells to radio-CDT in vitro and in vivo. In a subcutaneous 4T1 tumor model, the enhanced radio-CDT was confirmed by the increased contraction of cell nucleus, cell apoptosis and DNA double-strand breaking in the smallest tumor tissue obtained by the treatment of BBCD combined with RT. Furthermore, the results from the evaluation of cytotoxicity to normal cells, histological evaluation of major organs and blood biochemical analysis of the BBCD injected mice indicated that BBCD nanospheres were nontoxic to normal cells and tissues. Therefore, such well-designed BBCD nanospheres achieved the enhancement of radio-CDT by regulation of intracellular oxidative stress, which provided a novel prospective strategy for enhanced solid tumor complex therapy.

**Supplementary data**

Supplementary data are available at REGBIO online.
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Authors’ contributions
W.T. designed the study and performed most of the experiments, manuscript preparation. Z.T. performed the experiment of western blot assay and data analysis of RNA-sequencing, provided advises for experiment and assisted the manuscript preparation. F.W. assisted the manuscript preparation. K.M. assisted the animal experiment and manuscript revision. C.X. assisted to perform animal experiment. Y.S. assisted to perform cell experiments. Y.W. provided assistance for experiments and writing. Y.L. provided advises for writing. Z.Z. provided advises for writing. L.Z. provided advises for writing. J.W. assisted the manuscript preparation. K.M. assisted the animal experiment and manuscript revision. C.X. assisted to edit the manuscript. J.L. supervised the project and revised the manuscript. The final manuscript was reviewed and approved by all authors.

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