Use of Cardiac Computed Tomography and Magnetic Resonance Imaging in Case Management of Atrial Fibrillation with Catheter Ablation

Hee-Gone Lee, MD, Jaemin Shim, MD, PhD, Jong-il Choi, MD, PhD, Young-Hoon Kim, MD, PhD, Yu-Whan Oh, MD, PhD, Sung Ho Hwang, MD, PhD

1Department of Radiology, Korea University Anam Hospital, Seoul, Korea; 2Division of Cardiology, Department of Internal Medicine, Korea University Anam Hospital, Seoul, Korea

Atrial fibrillation (AF) is the most common arrhythmia associated with the risk of morbidity and mortality in clinical patients. AF is considered an arrhythmia type that develops and progresses through close connection with cardiac structural arrhythmogenic substrates. Since the introduction of catheter ablation-mediated electrical isolation of arrhythmogenic substrates, cardiac imaging indicates improved treatment outcome and prognosis with appropriate candidate selection, ablation catheter guidance, and post-ablation follow-up. Currently, cardiac computed tomography (CCT) and cardiovascular magnetic resonance (CMR) imaging are essential in the case management of AF at both pre-and post-procedural stages of catheter ablation. In this review, we discuss the roles and technical considerations of CCT and CMR imaging in the management of patients with AF undergoing catheter ablation.

Keywords: Computed tomography; Magnetic resonance imaging; Arrhythmia; Atrial fibrillation; Catheter ablation

INTRODUCTION

Atrial fibrillation (AF) is the most frequent arrhythmia and represents a growing health care problem worldwide (1). AF is characterized by the presence of an irregular ventricular interval and absence of distinct organized atrial activity (2). Studies on the pathophysiologic aspects of AF suggest that focal electrical activation induces and maintains AF through an arrhythmogenic substrate (3, 4).

Recent increase in the understanding of the mechanism and pathophysiology of AF has led to the development of catheter ablation to isolate electrically arrhythmogenic substrate of AF in the pulmonary vein (PV) and cardiac structures (5, 6). Haïssaguerre et al. (7) introduced the first approach to catheter ablation of AF by point ablation of PV in 1994. Since then, multiple approaches have been developed, including the segmental isolation of PV and circumferential ablation of cardiac structures (8). Recently, because of their invasiveness, advanced procedures of catheter ablation require careful decisions regarding appropriate candidate selection, catheter ablation strategies, and treatment monitoring because of their invasiveness (1).

With regard to successful catheter ablation of AF, cardiac computed tomography (CCT) and cardiovascular magnetic resonance (CMR) imaging enable appropriate candidate selection, guidance of the ablation catheter, and follow-up after catheter ablation (9, 10). This overview discusses the role of CCT and CMR imaging at the pre- and post-procedural stages of catheter ablation of AF.
Pre-Procedural Stage

Before catheter ablation of AF, CCT, and CMR imaging are performed for the purpose of comprehensive evaluation of the left atrium (LA), left atrial appendage (LAA), left ventricle (LV), and PVs.

Fig. 1. Function of LA during normal sinus rhythm and during AF. In normal sinus rhythm, LA function consists of 1) LA reservoir function at LV systole, 2) LA conduit function during early LV diastole, and 3) LA pump function at late LV diastole. In contrast to sinus rhythm, AF results in rapid and inconsistent heart motion, which may be associated with blurring heart contours on cardiac images. AF = atrial fibrillation, LA = left atrium, LV = left ventricle.

Fig. 2. Evaluation of LA volume by 3D techniques of CMR imaging. Transverse (A) and coronal (B) reformatting of CMR images helps determination of LA chamber areas. Sum of LA chamber areas (green) on thin slice CMR images (C) can be considered as measurement of actual LA volume. PVs and LAA are usually excluded in LA volume measurement using 3D LA model. CMR = cardiovascular magnetic resonance, LAA = left atrial appendage, LSPV = left superior pulmonary vein, PVs = pulmonary veins, RIPV = right inferior pulmonary vein, RSPV = right superior pulmonary vein, 3D = three-dimensional.
The LA

The LA is a bridge chamber between the LV and PVs (11). The presence of enlargement, dysfunction, and fibrosis of the LA indicates the progression of LA remodeling (12). Evaluation of the LA size, function, and fibrosis by CCT and CMR is performed to assess the LA remodeling in patients with AF.

The LA remodeling by chronic hemodynamic stress is a predictor of adverse cardiovascular outcome and AF recurrence after catheter ablation (13, 14). Severe enlargement and impairment of LA reflects the duration and severity of chronic hemodynamic stress to the LA. The LA size can be determined by the LA diameter, area, and volume (9, 15, 16), and the LA function can be represented commonly by the change of LA size during the cardiac cycle. In normal sinus rhythm, the LA has three mechanical functions: 1) LA reservoir function that reflects the LA filling during LV systole, 2) LA conduit function just before the onset of LA contraction, and 3) LA pump function during LV late diastole (16) (Fig. 1). Importantly, AF itself can cause loss of modulation and adaptation in LA function, which may interrupt the LA function. Electrocardiography (ECG) gating allows delineation of the changes of cardiac structures during the entire cardiac cycle by CCT and CMR (9, 10). In general, the LA diameter and area are measured in the four-chamber images at end-systolic phase of maximum value of the LA size. The LA volume can be measured using the area-length biplane or prolate ellipsoid method, both of which are less accurate than the modified Simpson method (16). Three-dimensional (3D) reformatting techniques for CCT and CMR imaging have improved the accuracy of LA volume quantification (16, 17) (Fig. 2).

The LA fibrosis is a hallmark of LA remodeling as well as an indicator of the arrhythmogenic substrate of AF (18). A prospective multicenter study demonstrates an association between the degree of the LA fibrosis and AF recurrence after catheter ablation (19). CMR imaging has the potential to delineate the LA fibrosis with 3D late-gadolinium enhancement (LGE) CMR technique (20) (Fig. 3). In LGE-CMR imaging, the LA fibrosis with accumulation of gadolinium contrast appears as bright-signal intensity of LGE on T1-weighted sequences. LGE-CMR imaging for the LA fibrosis determined with 3D LGE-CMR imaging.

Fig. 3. LA fibrosis determined with 3D LGE-CMR imaging.

3D LGE-CMR image (A) with excellent spatial resolution describes thin LA wall and hyperenhancement areas (arrows) in detail. Segmentation of thin LA wall with slice thickness of < 2 mm (B, C) can reconstruct 3D LA models (D-F) which show tissue composition of LA wall in basis of signal intensity of LGE (arrows, yellow foci). LGE = late-gadolinium enhancement, LIPV = left inferior pulmonary vein.
fibrosis needs high resolution and thin-section 3D images acquired during free breathing using both respiratory and ECG-gating (21). Oakes et al. (20) report that the LA-LGE correlates strongly with the level of low endocardial bipolar voltage as in the LA fibrosis. However, despite its useful potential, several technical limitations involving the limited spatial resolution of LGE-CMR imaging fluid filling, the underlying rhythm, and the imaging modalities etc., the complicated segmentation of the thin wall, and the various algorithms of signal intensity to define the LA fibrosis should be considered.

The LAA
The LAA as a remnant of the original embryonic LA has a pouch-like extension from the main body of the LA. The LAA is a common site of intracardiac thrombus formation and is significantly associated with the hemodynamic status of the LA.

During development of an AF episode, cardiac thrombus formation occurs commonly within the LAA of reduced contractility (22). The LAA thrombus is an absolute contraindication of catheter ablation (23). Transesophageal echocardiography (TEE) is a gold standard for identification of the LAA thrombus (24). Currently, CCT is recommended as a convenient alternative to TEE because the esophageal passage of the TEE probe may cause discomfort to the patient. Patel et al. (25) reported that CCT showed a negative predictive value of 100% for exclusion of the LAA thrombus. Although incomplete filling of contrast agent within the LAA may mimic the presence of thrombus on CCT images, addition of delayed computed tomography (CT) scan can improve the specificity to 99% in the diagnosis of the LAA thrombus (9).

The LAA is an actively contracting structure, which may

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**Fig. 4. Evaluation of LAA function by CMR imaging.** VENC CMR imaging can quantify blood flow through LAA ostium. Mechanically, active emptying of LAA can be represented mechanically by active contraction of LAA. It can be measured by peak blood flux (in mL/s) which develop at LV late diastole in sinus rhythm. VENC = velocity-encoded
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play an important role in cardiac hemodynamics. The LAA blood flow velocity through the LAA ostium is the preferred method to assess the LAA function. The four-phasic pattern of the LAA blood flow at sinus rhythm consists of the following: 1) Early diastolic passive emptying, 2) late diastolic active emptying, 3) the LAA relaxation, and 4) systolic reflection. The decreased LAA blood flow at late diastolic active emptying is associated with the LA hypertension and blood stasis which interrupt the blood flow from the LAA to LA chamber. Velocity-encoded (VENC) CMR is a cine phase contrast imaging technique that employs a bipolar gradient pulse to encode the velocity of moving protons (26). VENC-CMR imaging uniquely represents the late diastolic active emptying of LAA with quantification of blood flow through the LAA ostium (27) (Fig. 4). Hwang et al. (28) reported that the quantification of active emptying of LAA by VENC-CMR may be useful in assessing the LA hypertension in patients with AF.

The LV

The LV is the thickest of the four heart chambers and is located below the LA. The progression to permanent AF may have adverse effects on the myocardium of LV wall, which can result in remodeling of both the LA and LV. From the view-point of catheter ablation, the irreversible LV remodeling with myocardial fibrosis may reduce the effectiveness of treatment despite the termination of AF after catheter ablation. The LV dysfunction and fibrosis are considered as the major findings of the LV remodeling related to AF.

Reduced LV systolic function is associated with stroke in patients with AF (29). Beyond LV systolic function, LV diastolic dysfunction resulting from fibrotic infiltration of the myocardium may in turn perpetuate AF due to the resulting LA wall stress and remodeling (30). The LV function is traditionally expressed as LV end-diastolic volume, LV end-systolic volume, and LV ejection fraction, which can be assessed by CCT and CMR imaging (31).

LV myocardial fibrosis may occur secondary to irregular and fast LV contraction in the setting of long-standing AF (32). In general, the presence of LV myocardial fibrosis can be determined with LV-LGE of CMR imaging. Only 2% of patients with AF showed the presence of LV-LGE without myocardial infarction (33). Interestingly, the LV-LGE was a predictor of functional recovery of the LV in patients with AF and LV dysfunction undergoing catheter ablation (34).

Fig. 5. LV myocardial remodeling by CMR imaging in patient with AF.
Recent CMR technique provides assessment of myocardial ECV in LV wall derived from pre- and post-contrast T1 maps in patients with AF. In 40-year-old man with persistent AF, ECV map shows mean LV myocardial ECV of 31.69%. Usually, it has been widely accepted that mean LV myocardial ECV is less than 28% in healthy individuals without definite cardiomyopathy. ECV = extracellular volume fraction
The LV-LGE may be a significant independent predictor of AF recurrence after catheter ablation (35). In the setting of persistent AF, diffuse myocardial fibrosis of the LV wall may occur as a result of tachycardia-mediated cardiomyopathy (36) (Fig. 5). Recent CMR techniques allow the quantification of LV myocardial extracellular volume fraction (ECV), which is derived from pre- and post-contrast T1 measures (37). Neilan et al. (38) reported that the expansion of LV myocardial ECV through CMR imaging was associated with the risk of recurrent AF after catheter ablation.

The PVs

The myocardial muscle sleeves extending from the LA into the PVs are vital sources of AF triggers (23). The PVs are first target of catheter ablation-mediated electrical isolation (1). The typical anatomy comprises the four PVs with separate ostia; in contrast, the atypical PV anatomy mainly comprises an additional right middle PV or common ostium in the left PVs (15) (Fig. 6). The accessory ostia are smaller than normal (15). The PV ostial diameters undergo change during the cardiac cycle. The PVs are typically imaged at the cardiac late systolic phase, when they have the largest caliber.

The use of electroanatomic mapping systems to guide such catheter-based procedures requires CCT or CMR imaging to delineate the PV anatomy in detail (30). CCT images are acquired at end expiration to enable mapping in the electrophysiology laboratory. ECG gating is preferred to avoid motion artifacts. In patients with high heart rates and in large patients, retrospective ECG gating may be required. Non-ECG-gated helical scans are used in patients with AF and high heart rates (39). Motion artifacts with this technique are negligible and do not compromise the ability to make a diagnosis. Popular CMR technique for delineation of PVs and various cardiac structures is that of time-resolved magnetic resonance angiography (TR-MRA), which involves rapid sequential imaging of an anatomic volume during the luminal transit of a contrast bolus (40, 41) (Fig. 7). TR-MRA based on T1-weighted gradient echo

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**Fig. 6. PV anatomy and LA by CCT images.**
Isotropic voxel data from CCT scan can be reformatted into transverse (A) and coronal (B) multiplanar images. 3D volume rendering image (C) of CCT reveals stereoscopic view inside LA chamber and PV ostium. In 3D volume rendering images of PVs, typical anatomy comprises four PVs with separate ostia (D). Atypical PV anatomy mainly comprises common ostium for left PVs (arrow) (E) and additional right middle PV (arrow) (F). CCT = cardiac computed tomography.
sequence is designed based on sufficiently short repetition time to allow repeated imaging at temporal resolutions of 1–2 seconds per frame (40).

**Image Integration and Electroanatomic Mapping**

Using CCT and CMR volumetric data sets, a 3D cardiac model can be reconstructed. The 3D cardiac model can be referenced in the electrophysiology laboratory for catheter manipulation (42) (Fig. 8). 3D electroanatomic mapping based on imaging volumetric data sets permits tracking of catheter movement and more precise localization of ablation points. Anatomic shells on the models of the cardiac atria are created by moving the catheter along the walls of the 3D cardiac model and recording multiple catheter positions (9, 43). Electrograms and points of interest can be displayed on the 3D electroanatomic mapping. It has become apparent that the use of 3D anatomic mapping with image integration may reduce procedure time and shorten radiation exposure (43). However, previous randomized studies showed no significant improvement of clinical outcome by image integration in catheter ablation of AF (42, 44).

**Post-Procedural Stage**

Regardless of the AF termination after catheter ablation, the catheter ablation of AF itself can have various consequences on cardiac structures such as the ablation-induced simple scar, shrinkage of the LA chamber, enlargement of the LAA, and critical complications. After the catheter ablation of AF, post-procedural CCT and CMR imaging can be performed for assessment of the appropriateness of catheter ablation and early detection of the ablation-related complications.

**Ablation-Induced LA Scar and the LA Reverse Remodeling**

Generally, the catheter ablation of AF produces the LA scar along the ablation line as well as the termination of

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**Fig. 7. Evaluation of PV by CMR imaging.**

TR-MRA shows sequential contrast enhancement of large vessels from PA (A), through LA and aorta (B), to IVC (C). Multi-phase images by TR-MRA allows reconstruction of 3D models including CS, IVC, right atrium and LA. CS = coronary sinus, IVC = inferior vena cava, PA = pulmonary artery, TR-MRA = time-resolved magnetic resonance angiography.

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**Fig. 8. Electroanatomic mapping.**

Electroanatomic maps can help guide catheters (arrow) (A), reveal process of ablation lines (B), and fuse between LA model from cardiac image data and shell of electrophysiologic study (C) during catheter ablation of AF.
AF. These pathophysiologic processes by catheter ablation can arrest the LA remodeling, and subsequently result in shrinkage of the LA chamber as the LA reverse remodeling. Therefore, the LA reverse remodeling and ablation-induced LA scar are typical changes of the LA structure after the catheter ablation of AF.

Radiofrequency energy generated from the catheter ablation procedure causes permanent lesions as the ablation line surrounding the LA wall with circumferential arrhythmogenic substrate (21). The ablation-induced LA scar by ablation line shows the myocardial stasis of gadolinium contrast agent with ECV expansion. Especially, LGE-CMR imaging enables direct identification and quantification of the ablation line by delayed stasis of gadolinium in the LA wall (45) (Fig. 9). The presence of gaps from incomplete ablation lines has been implicated as one of the reasons for the recurrence of AF. LGE-CMR imaging for the identification of incomplete ablation line by non-invasive approach has useful potential in both the assessment of the catheter ablation efficiency and guidance of the second catheter ablation procedure (46, 47).

Catheter ablation commonly results in shrinkage of the enlarged LA chamber defined as the reverse LA remodeling (14, 48). Improvement of the LA function after catheter ablation represents the increase in LA contractility with achievement of normal sinus rhythm. However, the LA

![Fig. 9. Ablation-induced LA scar by 3D LGE-CMR imaging.](https://doi.org/10.3348/kjr.2018.0774)

Post-procedural 3D LGE-CMR image shows thick LA wall areas of bright signal intensity (arrowheads) due to ablation-induced LA scar near RSPV. Post-procedural 3D LA model by LGE reveals ablation lines (arrowheads) surrounding LA antrum for electrical isolation of RSPV.
reverse remodeling with loss of LA contractility can be caused by the ablation-induced LA scar itself. Although the LA reverse remodeling has been considered as a characteristic of successful catheter ablation, the degree of LA reverse remodeling is not associated with the recurrence of AF after catheter ablation.

Enlargement of the LAA

Paradoxically, there is enlargement of the LAA after the catheter ablation of AF (49) (Fig. 10). Recent study using CMR imaging reports that the volume of the LAA increases by > 20% after the catheter ablation of AF as compared to that before treatment (50). Enlargement of

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**Fig. 10. Enlargement of LAA after catheter ablation of AF.** Post-procedural 3D LGE-CMR image shows thick LA wall areas of bright signal intensity (arrows) due to ablation-induced LA scar near ostium of LAA. Compared with pre-procedural CMR images, dimension of LAA ostium (red box) was decreased although chamber of LAA was enlarged. Volume of LAA increased from 49.6–61.7 mL after catheter ablation of AF.
the LAA after catheter ablation may develop due to the AF recurrence, stiff LA wall by the ablation-induced LA scar, and inappropriate contraction of the LAA (49). Eventually, the development of significant enlargement of the LAA suggests worsening hemodynamics between the LA chamber and LAA (51). Although the unstable hemodynamics in the enlarged LAA is a critical risk factor of thrombus formation, the clinical significance of routine monitoring of the LAA after catheter ablation is still uncertain.

**Pulmonary Vein Stenosis**

Pulmonary venous stenosis (PVSt) is defined as the reduction in PV diameter of > 50% compared to that before the catheter ablation of AF (52). PVSt may result in focal lung edema, veno-occlusive disease, lung parenchymal hemorrhage, and venous thrombosis (53) (Fig. 11). To confirm the diagnosis, CT is the technique of choice, although CMR provides the same information without the need for radiation or iodinated contrast (54). Chest CT imaging has an important role to diagnose PVSt and evaluate risk factors, such as the PV ostia and left inferior PV location. Balloon angioplasty and stent insertion can be applied to treat patients with significant PVSt after the catheter ablation of AF (55).

**Atrioesophageal Fistula**

Atrioesophageal fistula (AEF) after catheter ablation is rare, but fatal complication from cerebrovascular events due to air embolism (56). Extensive catheter ablation targeting the PVs and posterior LA wall may increase the prevalence of AEF. Esophagus is most susceptible to injury because it is closest to the areas of endocardial ablation. AEF usually develops

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Fig. 11. PV stenosis in 50-year-old male who underwent catheter ablation of AF.

Transverse chest CT image (A) shows interstitial edema and consolidation of left lung lower lobe. Chest CT image (B) with mediastinal window set shows interstitial edema and luminal narrowing of LIPV (arrow). Conventional angiography (C) also shows focal narrowing of LIPV as PV stenosis (arrow). Six-month follow-up cardiac CT image (D) shows in-stent restenosis (arrow) after stent insertion for PV stenosis.
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at 1–4 weeks after the catheter ablation of AF (1). TEE and esophagoscopy are contraindicated in case of suspected AEF. Contrast-enhanced chest CT is the imaging modality of choice, and the specific CT findings of AEF include air-bubbles at the mediastinum or LA near the esophagus (57) (Fig. 12). Immediate surgery is needed to prevent serious and fatal outcomes due to air and food embolism.

In conclusion, catheter ablation of AF is a current personalized case management approach in patients diagnosed with AF. CCT and CMR imaging are modalities that can help identifying patients at high risk for AF progression, can help plan treatment strategy in patients diagnosed with AF, and can evaluate the result of catheter ablation. Since these modalities are essential tool for safe and efficient catheter ablation AF, it is important to understand their roles, technical characteristics, and performance in the management of AF with catheter ablation.

Conflicts of Interest

The authors have no potential conflicts of interest to disclose.

ORCID iDs

Sung Ho Hwang
https://orcid.org/0000-0003-1850-0751

Hee-Gone Lee
https://orcid.org/0000-0002-2729-9925

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