The cortical signature of symptom laterality in Parkinson’s disease

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\begin{abstract}
Patients with Parkinson’s disease (PD) often present with unilateral motor symptoms that eventually spread to the other side. This symptom lateralization is diagnostically important, as it serves to distinguish PD from other motor disorders with overlapping symptom profiles. Further, recent studies have shown that the side of symptom onset is important for prognosis, as there are differences in the rate of disease progression and the incidence of secondary symptoms between right- and left-dominant (RD, LD) patients. Physiologically, previous studies have shown asymmetrical decline in structure and metabolism throughout the basal ganglia, although connecting this directly to motor function has been difficult. To identify the neurophysiologically basis of symptom laterality in PD, we recorded magnetoencephalography (MEG) during left- and right-hand movement paradigms in patients with PD who exhibited either RD or LD symptomatology. The beta oscillations serving these movements were then imaged using beamforming methods, and we extracted the time series of the peak voxel in the left and right primary motor cortices for each movement. In addition, each patient’s symptom asymmetry was quantitated using the Unified Parkinson’s Disease Rating Scale (UPDRS), which allowed the relationship between symptom asymmetry and neural asymmetry to be assessed. We found that LD patients had stronger beta suppression during movement, as well as greater post-movement beta rebound compared to patients with RD symptoms, independent of the hand that was moved. Interestingly, the asymmetry of beta activity during right-hand movement uniquely correlated with symptom asymmetry, such that the more LD the symptom profile, the more left-lateralized (i.e., contralateral to movement) the beta response; conversely, the more RD the symptom profile, the more right-lateralized (i.e., ipsilateral to movement) the beta response. This study is the first to directly probe the relationship between symptom asymmetry and the laterality of neural activity during movement in patients with PD, and suggests that LD patients have a fundamentally different and more “healthy” oscillatory pattern relative to RD patients.

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\end{abstract}

1. Introduction

Parkinson’s disease (PD) is a neurodegenerative disorder characterized by muscle rigidity, bradykinesia, resting tremor, impaired posture and balance, and speech and writing changes (Jankovic, 2008). PD initially emerges as a unilateral disorder, such that symptoms begin on one side of the body and spread to the other, although symptoms continue to be worse on the initially-affected side throughout the disease process (Djaldetti et al., 2006; Haaxma et al., 2010; Hoehn and Yahr, 2001; Lee et al., 1995; Riederer and Sian-Hulsmann, 2012; Uitti et al., 2005). This lateralization is diagnostically important, as it allows PD to be distinguished from other neurodegenerative disorders including essential tremor (Thenganatt and Louis, 2012), multiple system atrophy, and supranuclear palsy (Suchowersky et al., 2006). Interestingly, the side initially affected in PD has been recently associated with symptom trajectories. Indeed, a large-scale prospective study showed that patients with a right-dominant (RD) symptom profile had significantly more rapid progression of motor symptoms compared to those with a left-dominant (LD) symptom profile (Baumann et al., 2014). Patients with RD symptoms also showed significantly decreased muscle strength on both sides of the body compared to healthy controls, whereas LD patients showed no such differences (Frazzitta et al., 2015). Finally, LD symptomatology has been associated with longer disease duration, indicative of an extended period of survival after diagnosis, as well as delayed ambulatory inhibition compared to RD symptomatology (Munhoz et al., 2013). Taken together, these findings suggest that the side of symptom onset may hold important implications for predicting symptom trajectory in PD, and thus formulating prognoses.
Nonetheless, the nature of symptom asymmetry in PD, especially the degree of asymmetry (i.e., how unilateral or bilateral symptoms present) and its neurophysiological origin, remains to be characterized.

Various studies have demonstrated asymmetrical subcortical structure and function in patients with PD (Abe et al., 2000; Choe et al., 1998; Eidelberg et al., 1990; Kempster et al., 1989; Morrish et al., 1995; Rinne et al., 1993). Overwhelmingly, researchers have found that the substantia nigra (SN) and putamen contralateral to the more affected side have greater degeneration and reduced dopamine uptake compared to homologous structures on the ipsilateral side. For example, Choe et al. (1998) used 1H-MRS to determine various metabolite levels in the SN and putamen of patients with unilateral PD. They found decreased N-acetylaspartate to creatine ratios (NAA/Cr; indicative of neuronal impairment) in both structures contralateral to the affected side, irrespective of whether patients were LD or RD (Choe et al., 1998). Similarly, many PET studies have demonstrated reduced endogenous dopamine, as well as reduced dopamine uptake, in the basal ganglia contralateral to the affected side, and that this asymmetry persists when Parkinson’s symptoms become bilateral (Bohnen et al., 2006; Lin et al., 2014; Rinne et al., 1993). Most recently, diffusion tensor imaging in patients with PD has shown reduced fiber integrity throughout the nigrostriatal pathway, but especially contralateral to the more affected side (Wang et al., 2015; Zhang et al., 2015). In contrast to this subcortical work, very few studies have investigated potential neural asymmetries in the neocortex of patients with PD (Hall et al., 2014; Pollok et al., 2012). Overall, these studies show differential resting and movement-related neural activity in the hemisphere contralateral to the more affected side compared to the ipsilateral hemisphere, which suggests that these asymmetries transcend basal ganglia structures. However, these studies did not distinguish between RD and LD patients and thus, did not investigate whether the strength of such asymmetries might differ between these subtypes of patients with PD. Further, no study to date has connected the degree of symptom laterality to neural laterality in subcortical or cortical regions. Given the heterogeneity of symptom expression in PD and the substantial differences between RD and LD patient prognoses, understanding this relationship may provide critical new insight to disease progression.

A widely replicated finding in patients with PD undergoing deep brain stimulation (DBS) surgery is the presence of pathological beta activity (14–30 Hz) throughout the basal ganglia motor circuit (Brown, 2007; Cassidy et al., 2002; Hammonds et al., 2007; Little and Brown, 2014; Litvak et al., 2011). Such beta activity is known to be critical for successful movement execution and its inherent time course has been well characterized. Briefly, about 1.0 s prior to movement onset there is a strong decrease in cortical beta activity, which has been termed the beta event-related desynchronization (ERD) response. This response appears to be generated by the bilateral primary motor cortices (stronger contralateral to movement), with weaker activity in the parietal, premotor, and supplementary motor areas (Gaetz et al., 2010; Heinrichs-Graham et al., 2016; Heinrichs-Graham and Wilson, 2016, 2015; Heinrichs-Graham et al., 2014b; Jurkiewicz et al., 2006; Wilson et al., 2014; Wilson et al., 2013; Wilson et al., 2010; Wilson et al., 2011). Approximately 0.5 s after movement offset, there is a strong resynchronization of beta activity that lasts approximately 2.0 s, termed the post-movement beta rebound (PMBR; Gaetz et al., 2010; Heinrichs-Graham et al., 2014b; Jurkiewicz et al., 2006; Wilson et al., 2010, 2011)). The beta ERD and PMBR have been reliably associated with movement planning/selection and active motor termination operations, respectively (Alegre et al., 2008; Alegre et al., 2004; Doyle et al., 2005; Grent’s-Jong et al., 2014; Heinrichs-Graham and Wilson, 2015, 2016; Solis-Escalante et al., 2012; Tzagarakis et al., 2010), and are strongly modulated in the healthy aging brain (Heinrichs-Graham and Wilson, 2016; Rossiter et al., 2014). Importantly, recent work from our laboratory using noninvasive magnetoencephalography (MEG) has demonstrated pathologically-reduced beta activity in the motor cortices of patients with PD compared to healthy controls, both at rest and during transient movement (Heinrichs-Graham et al., 2014a, 2014b). Specifically, we found reduced beta ERD (i.e., weaker suppression relative to baseline) and marginally reduced PMBR amplitude (i.e., less increase from baseline) in patients with PD compared to healthy controls. Taken together, these data indicate that beta oscillatory activity is critical to the dysfunction seen in motor circuits, and the overall pathophysiology of PD.

The primary goal of the current study was to determine whether symptom laterality in patients with PD (i.e., LD or RD) is associated with distinct aberrations in motor-related beta activity. To this end, we collected high-density MEG to examine oscillatory activity during two movement tasks in right-handed patients with PD who had either a LD or RD symptom profile. Movement-related beta oscillatory responses were then imaged using beamforming, and the level of symptom asymmetry was quantified using the Unified Parkinson’s Disease Rating Scale (UPDRS). These data were then used to evaluate the relationship between neuronal activity and symptom asymmetry. Consistent with recent clinical studies showing differences in LD/RD patients, we hypothesized that patients who were LD would exhibit significantly stronger (i.e., more negative) beta ERD activity, as well as stronger (i.e., more positive) PMBR activity, compared to patients who were RD. The directionality of this hypothesis is in line with prior neurophysiological research showing that patients with PD have reduced motor-related responses compared to healthy controls (Heinrichs-Graham et al., 2014b; Pollok et al., 2012); thus, it is intuitive in this population that stronger motor-related responses are indicative of a “healthier” motor system. Secondly, we hypothesized that the pattern of neural asymmetry would reflect the pattern of symptom asymmetry across the two patient groups.

2. Methods

2.1. Subject selection and behavioral testing

We studied 27 right-handed adults (4 females) with well-documented PD. Four participants were excluded from analysis due to artifacts in their MEG data (2 participants) or no significant movement-related oscillatory response (1 participant). An additional participant was excluded due to the discovery of exclusionary criteria post-enrollment. The mean age of the remaining patients was 64.74 years (range: 52–78 years; see Table 1). All participants had been prescribed a regularly-monitored and unchanged dosage of antiparkinsonian medication for at least 2 months prior to study enrollment, and had showed a satisfactory clinical response to the particular antiparkinsonian medication(s). Exclusionary criteria included any medical illness affecting CNS function, neurological disorder(s) besides PD, history of head trauma, and current substance abuse. After complete description of the study to participants, written informed consent was obtained following the guidelines of the University of Nebraska Medical Center’s Institutional Review Board, which approved the study protocol.

Parkinsonism was measured by a certified rater using either the UPDRS (12 patients) or the Movement Disorders Society-sponsored revision of the UPDRS (MDS-UPDRS (Goetz et al., 2007), 11 patients) in the practically-defined “off” state, which means following at least a 12-hour holiday from antiparkinsonian medications. In order to identify left- or right-dominance of symptoms, scores from each item on the (MDS-)UPDRS Part III that contained both a right and a left side component (e.g., right upper limb resting tremor, left upper limb resting tremor) were extracted, which provided left and right motor subscores for each individual. Symptom asymmetry was calculated using each patient’s motor subscores by subtracting the total symptom score from the right side from the total symptom score from the left side. Negative values of symptom asymmetry (\(L_R\)) indicated LD of symptoms, while positive values indicated RD. Using this calculation, we divided our patient group by asymmetry of symptoms, such that 12 patients with PD exhibited symptoms that were LD (1 female), and 11 had symptoms...
Table 1
Clinical and demographic characteristics.

| Subject ID | Age (yrs) | Sex | Disease duration (yrs) | PD medications (type, dose) | [MDS]-UPDRS-III |
|------------|-----------|-----|------------------------|-----------------------------|-----------------|
| 1          | 62        | M   | 4                      | Pram (4.5 mg), Ras (1 mg)   | 22              |
| 2          | 70        | M   | –                      | Pram (1.5 mg), CD/LD (25/100 mg) | 17              |
| 3          | 52        | M   | 9                      | CD/LD, Rop                  | 62              |
| 4          | 61        | M   | –                      | Rop (1 mg)                  | 15              |
| 5          | 60        | M   | 1                      | Rop (1 mg)                  | 27              |
| 6          | 72        | F   | 9                      | Rop                        | 13              |
| 7          | 64        | F   | 8                      | Ras (1 mg) CD/LD (25/100 mg) | 34              |
| 8          | 67        | M   | 3                      | CD/LD (25/100 mg)           | 23              |
| 9          | 69        | M   | –                      | CD/LD (50/200 mg)           | 52              |
| 10         | 69        | M   | –                      | CD/LD                       | 37              |
| 11         | 52        | M   | 6                      | Rop (8 mg)                  | 14              |
| 12         | 64        | M   | 7                      | CD/LD (25/100 mg), Aman      | 28              |
| 13         | 75        | M   | 8                      | CD/LD (25/100 mg)           | 29              |
| 14         | 64        | M   | 7                      | CD/LD (10/100 mg), Rot (8 mg) | 53              |
| 15         | 61        | M   | 8                      | CD/LD (25/100 mg), Pram (1.5 mg), Sel (2 mg) | 35              |
| 16         | 55        | M   | 6                      | CD/LD (25/100 mg)           | 21              |
| 17         | 78        | F   | 16                     | CD/LD (25/100 mg)           | 36              |
| 18         | 73        | M   | 8                      | CD/LD (25/100 mg), Rot (4 mg) | 54              |
| 19         | 55        | M   | 9                      | Pram (1 mg), CD/LD (25/100 mg), Sel (5 mg) | 60              |
| 20         | 66        | M   | 5                      | Rop (3 mg), Ras (1 mg)      | 40              |
| 21         | 61        | M   | 3                      | CD/LD (25/100 mg), Pram (1 mg) | 57              |
| 22         | 67        | M   | 5                      | CD/LD (25/100 mg)           | 36              |
| 23         | 72        | M   | 8                      | CD/LD (25/100 mg)           | 39              |
| 24         | 54        | F   | 6                      | Pram (4.5 mg), CD/LD (25/100 mg) | 27              |
| 25         | 76        | M   | 4                      | Ras (1 mg), CD/LD (50/200 mg) | 35              |
| 26         | 57        | M   | 3                      | Aman (100 mg), CD/LD (25/100 mg) | 31              |
| 27         | 75        | M   | –                      | Pram (0.5 mg), CD/LD (25/100 mg) | 17              |

Notes: Pram = pramipexole; Ras = rasagline; CD/LD = carbidopa/levodopa; Rop = ropinirole; Aman = amantadine; Sel = selegiline; Rot = rotigotine.
* Excluded from analysis.

that were RD (2 females). These groups were matched on sex, age, and whether their Parkinsonism had been rated using the UPDRS or the MDS-UPDRS (UPDRS: 6 of 12 LD patients; 5 of 11 RD patients). There was no significant difference in the sum of left and right UPDRS subscores between LD and RD patients with PD, t(21) = 1.749, p = 0.095, which ensures that disease severity was uniform between groups.

2.2. Experimental paradigm

All patients were scheduled for MEG early in the morning (i.e., 07:30–08:00) and a minimum of 12 h since their last dose of antiparkinsonian medication. During MEG recording, participants were seated with both arms resting on a table attached to their chair. Dual-plane accelerometer chips (Analog Devices Inc., model: ADXL103) were attached to each index finger to precisely quantify movement onset and the rate of acceleration (see Section 2.4), and to continuously monitor for intermittent tremor. Participants were instructed to fixate on a cross hair presented centrally and to perform a single tap of the right (or left) index finger each time a dot reached the 12 o’clock position (Fig. 1). This dot completed one full revolution, around a clock-like circle without numbers or tick marks every 6 s, which constituted one trial (Heinrichs-Graham et al., 2014b; Wilson et al., 2014, 2013, 2010). Left and right index finger movements were completed in separate blocks, with the order being randomized between participants. Each patient performed at least 105 trials for each task, and the total recording time was ~22 min. Of note, 19 patients (10 LD, 9 RD) completed both tasks, while the other four (2 LD, 2 RD) performed only the right finger-tapping task.

2.3. MEG data acquisition & coregistration with structural MRI

All recordings were conducted in a one-layer magnetically-shielded room with active shielding engaged. Neuromagnetic responses were sampled continuously at 1 kHz with an acquisition bandwidth of 0.1–330 Hz using an Elekta MEG system with 306 magnetic sensors (Elekta, Helsinki, Finland). Using MaxFilter (v2.2; Elekta), MEG data from each patient were individually corrected for head motion and subjected to noise reduction using the signal space separation method with a temporal extension (Taulu and Simola, 2006; Taulu et al., 2005). Each participant’s MEG data were coregistered with structural T1-weighted MRI data prior to source space analyses using BESA MRI (Version 2.0). Structural MRI data were aligned parallel to the anterior and posterior commissures and transformed into standardized space. After beamformer analysis, each subject’s functional images were also transformed into standardized space using the transform applied to the structural MRI volume and spatially resampled.

2.4. MEG time-frequency transformation and statistics

Cardiac artifacts were removed from the data using signal-space projection (SSP), which was accounted for during source reconstruction (Usui-talo and Ilmoniemi, 1997). The continuous magnetic time series was divided into epochs of 4.5 s duration, with 0.0 s defined as movement onset and the baseline defined as the −2.0 to −1.2 s time window (i.e., before movement onset). Movement onset was defined using the dual-plane accelerometers, which were attached to each index finger and digitized along with the MEG data at 1 kHz. The onset of movement was determined and quantified by a sharp increase in the amplitude of the accelerometer signal attached to the index finger being moved. Epochs containing artifacts were rejected based on a fixed threshold method, supplemented with visual inspection.
Artifact-free epochs were transformed into the time-frequency domain using complex demodulation (resolution: 2.0 Hz, 25 ms) and the resulting spectral power estimations per sensor were averaged over trials to generate time-frequency plots of mean spectral density. These sensor-level data were normalized by dividing the power value of each time-frequency bin by the respective bin’s baseline power, which was calculated as the mean power during the $-2.0$ to $-1.2$ s time period. The specific time-frequency windows used for imaging were determined by statistical analysis of the sensor-level spectrograms. Each data point in the spectrograms was initially evaluated using a mass univariate approach based on the GLM. To reduce the risk of false positive results, a two-stage procedure involving nonparametric permutation testing was followed to control for Type 1 error. In the first stage, one-sample t-tests were conducted on each data point and the output spectrogram of t-values was thresholded at $p < 0.05$ to define time-frequency bins containing potentially significant oscillatory deviations across all participants. In stage two, time-frequency bins that survived the threshold were clustered with temporally and/or spectrally neighboring bins that were also above the $(p < 0.05)$ threshold, and a cluster value was derived by summing all of the t-values of all data points in the cluster. Nonparametric permutation testing was then used to derive a distribution of cluster-values and the significance level of the observed clusters (from stage one) was tested directly using this distribution (Ernst, 2004; Maris and Oostenveld, 2007). For each comparison, at least 10,000 permutations were computed to build a distribution of cluster values. Based on these analyses, the time-frequency windows that contained significant oscillatory events across all participants and corresponded to those of a priori interest (e.g., beta ERD, PMBR) were subjected to the beamforming analysis. Further details of this method and our processing pipeline can be found in recent papers (Heinrichs-Graham et al., 2014b; Wilson et al., 2014, 2015).

2.5. MEG imaging

Cortical networks were imaged through an extension of the linearly constrained minimum variance vector beamformer (Gross et al., 2001), which employs spatial filters in the frequency domain to calculate source power for the entire brain volume. The single images were derived from the cross spectral densities of all combinations of MEG gradiometers averaged over the time-frequency range of interest, and the solution of the forward problem for each location on a grid specified by input voxel space. Following convention, the source power in these images was normalized per participant using a separately averaged pre-stimulus noise period of equal duration and bandwidth (Hillebrand et al., 2005). MEG pre-processing and imaging used the Brain Electrical Source Analysis (BESA version 6.0) software. Normalized source power was computed for the selected time-frequency bands over the entire brain volume per participant at $4.0 \times 4.0 \times 4.0$ mm resolution. Beamformer images were then averaged across participants, and coordinates corresponding to peak responses were identified for the left and right hand individually. We extracted virtual sensors corresponding to the peak voxel per region and task, and these were used to statistically evaluate neuronal activity in these brain regions between groups.

2.6. Statistical analysis

Oscillatory power for each response was extracted from the virtual sensors by averaging the total power over the same time-frequency bins that were determined previously by statistical analysis of the sensor-level data (see below). A linear mixed-model design was then employed in order to determine the relationship between side of movement (left or right index finger), hemisphere of response (contralateral or ipsilateral to movement), and affected side (LD or RD). Briefly, a linear mixed-model offers advantages over the general linear model, especially in cases of repeated-measures designs of unbalanced data (Jiang, 2007). Finally, correlations were computed to further resolve the relationship between variables on the patient level. All statistical analyses were performed using IBM SPSS Statistics (Release 23.0.0, Armonk, NY).

3. Results

All participants successfully completed the tasks. Across both groups, an average of 94.68 (SD: 10.44) artifact-free trials were used in the right hand analysis and 97.32 (SD: 9.32) were used in the left hand analysis. There were no significant differences between LD and RD groups on the number of trials used in either analysis, right hand: $t(20) = 0.420, p = 0.679$, left hand: $t(17) = 1.030, p = 0.318$. There were also no significant differences within group in the number of trials used per hand for those who performed both tasks, $t(17) = 0.548, p = 0.591$.

3.1. Sensor-level results

Sensor-level time-frequency spectrograms indicated the typical response pattern of peri-movement beta desynchronization followed by a PMBR in all patients. These spectrograms were statistically examined using one sample t-tests (across both groups) to derive the precise time-frequency bins for beamforming and subsequent virtual sensor analyses. Significant peri-movement beta ERD was found in a large number of sensors near sensorimotor regions in the 14–24 Hz range from about 1.0 s before movement onset until about 0.3 s after movement onset ($p < 0.0001$, corrected). There was also a significant beta synchronization (i.e., PMBR) that extended from about 0.5 s to 2.0 s after movement ($p < 0.0001$, corrected). To identify the neural origin of the beta ERD and PMBR, we imaged the time-frequency bin that showed the highest amplitude responses across all participants (Beta ERD: $-0.3$ s to 0.2 s, 14–24 Hz; PMBR: 0.7 to 1.5 s, 14–24 Hz).

3.2. Neuroanatomical results

Analysis of the beamformer images of each group revealed strong desynchronization and subsequent rebound both centered on the motor hand knob region (Yousry et al., 1997) of the precentral gyrus contralateral to movement, as well as a smaller cluster in the same region of the ipsilateral hemisphere (Fig. 2). Peaks for the beta ERD and PMBR were distinct, in agreement with prior literature (Fry et al., 2016; Jurkiewicz et al., 2006). The beta ERD time courses for the peak voxel per hemisphere (ipsi- and contralateral) and hand (i.e., left and right) are shown in Fig. 3; the time series of the PMBR responses followed a very similar trajectory to those of the beta ERD activity. A linear mixed model was employed to determine the effects of and interactions between affected side (LD, RD), side of movement (left, right), and hemisphere (contralateral, ipsilateral) on beta ERD power and PMBR power, separately. The model of beta ERD power was significant, $F(7,74) = 5.433, p < 0.001$, and there was a significant main effect for each factor (affected side: $F(1,74) = 11.119, p = 0.001$); hand: $F(1,74) = 16.023, p < 0.001$; hemisphere: $F(1,74) = 6.491, p = 0.013$). No interactions between the variables were significant. Follow-up testing of model contrasts revealed that LD patients had significantly stronger (i.e., more negative) beta ERD responses, regardless of which finger was moved or hemisphere of response ($t = 3.064, p = 0.003$). Further, beta ERD responses were stronger on the side contralateral relative to the ipsilateral to the movement ($t = 2.337, p = 0.022$). Finally, both LD and RD patients showed stronger beta ERD in both the contralateral and ipsilateral precentral gyrus when moving their left finger compared to their right finger ($t = 3.861, p < 0.001$). The linear mixed model of PMBR power was marginally significant, $F(7,74) = 1.926, p = 0.077$. The main effect of affected hand was significant, $F(1,74) = 8.464, p = 0.005$, but no other effects or interactions were significant (though a three-way interaction (affected hand, hand moved, and hemisphere) was marginal, $F(1,74) = 3.815, p = 0.055$). Follow-up contrast testing
showed that LD patients exhibited stronger PMBR responses compared to RD patients, regardless of hemisphere or finger moved ($t = 2.266$, $p = 0.027$). Full results of each model can be found in Table 2.

Finally, we calculated the partial correlation between neural asymmetry indices and symptom asymmetry, controlling for symptom severity (i.e., total UPDRS score from left and right subscores). We found a significant correlation between right hand beta ERD asymmetry and symptom asymmetry, $r(15) = 0.530$, $p = 0.029$, such that the more LD the symptom profile, the more left-lateralized the beta ERD, and in contrast, the more RD the symptom profile, the more right-lateralized the beta ERD response (see Fig. 4). We performed the same calculations using the PMBR amplitude from the left and right precentral gyri to determine the asymmetry of the PMBR response; values from the left hand correlated with symptom asymmetry, $r(15) = 0.486$, $p = 0.048$, such that the more right-lateralized the symptom profile, the more right-lateralized (i.e., contralateral to movement) the PMBR response, and vice versa. No other correlations were significant.

4. Discussion

Our goal in this study was to identify the motor-related neural correlates of symptom asymmetry in patients with PD. We found that patients with LD symptomatology had significantly greater peri-movement beta ERD power (i.e., more negative relative to baseline) as well as greater PMBR activity (i.e., more positive relative to baseline) compared to patients with RD symptomatology, regardless of whether they were moving their right (less affected) or left (more affected) hand. Further, there was a significant correlation between symptom asymmetry and neural asymmetry for the right hand, such that the more left-lateralized the symptom profile, the more left-lateralized the beta ERD activity (i.e., greater beta ERD contralateral to movement), and the more right-lateralized the symptom profile, the more right-lateralized the beta ERD (i.e., greater beta ERD ipsilateral to movement). Below, we discuss the implications of these findings for understanding the cortical basis of symptom laterality in PD, and the recent discussions of distinct clinical outcomes among LD and RD patients.

Prior behavioral data suggests that patients with PD who have a LD symptom profile have a more favorable symptom trajectory than those with a RD profile, including a shallower symptom trajectory, longer disease duration, reduced muscle fatigue, and delayed ambulatory depletion (Baumann et al., 2014; Frazzitta et al., 2015; Munhoz et al., 2013). Despite the growing body of literature suggesting a behavioral dissimilarity between LD and RD patients with Parkinson’s, the underlying neural mechanisms remain largely unknown. To at least some extent, this is because most studies to date have combined patients with LD and RD symptomatology, in order to focus on the more general effects of PD on brain structure and function. Our previous MEG investigation compared beta ERD and PMBR amplitude in patients with PD compared to healthy controls during the same finger-tapping movement of the right hand (Heinrichs-Graham et al., 2014b). We found that patients with PD had abnormally reduced beta ERD amplitude prior to and during movement, as well as marginally reduced PMBR amplitude following movement termination, compared to healthy age-matched adults (Heinrichs-Graham et al., 2014b). These results provided preliminary evidence that movement-related beta oscillatory activity may be a good candidate by which to investigate differences within the PD population. Indeed, in accordance with our hypothesis and in line with these findings, the current results show that patients who exhibited a LD symptom profile have significantly stronger beta ERD and PMBR responses (i.e., more healthy) during movement compared to those with RD symptomatology, regardless of whether they were moving their more-affected or less-affected side. This is in agreement with one recent single-photon emission computed tomography (SPECT) study by Scherfler and colleagues that examined levels of striatal dopamine transporter uptake between patients with PD and healthy controls, as well as between patients with LD and RD symptomatology (Scherfler et al., 2012). This study showed a reduction in dopamine transporter uptake between patients with PD and healthy controls, and that this reduction was more targeted to the left putamen than the right (Scherfler et al., 2012). Importantly, total dopamine uptake depletion in the left and right putamen was significantly greater in patients with RD compared to LD symptom profiles (Scherfler et al., 2012). Taken together, it is possible that the greater dopamine depletion in the putamen of...
patients with RD relative to LD symptomatology strongly alters the local physiology, and that these alterations disrupt brain activity in higher-order structures like the motor cortex, as evidenced by the reduction in beta ERD and PMBR power in the current study.

There is a wealth of positron emission tomography (PET) and magnetic resonance spectroscopy (MRS) data showing resting-state metabolic and dopamine receptor asymmetries in the basal ganglia of patients with PD, which correlate with the degree of symptom asymmetry (Abe et al., 2000; Choe et al., 1998; Eidelberg et al., 1990; Morrish et al., 1995; Rinne et al., 1993). However, few studies have examined aberrations in cortical neurophysiology while controlling for, but not directly investigating differences in, symptom laterality in patients with PD (Hall et al., 2014; (Pollok et al., 2012; Wu et al., 2015). Thus, the relationship between this subcortical asymmetry and cortical dynamics was largely unknown. In the current study, we found that there was a significant relationship between the asymmetry of beta ERD power during right hand movements in the contralateral and ipsilateral motor cortices and symptom asymmetry (LD, RD). We were initially surprised that this relationship was unique to the right hand, but we suggest that this might be due to the overall difference in beta ERD asymmetry between the left and right hands across patient groups. Basically, our results suggest that the healthy pattern of neural physiology (i.e., bilateral activation with greater activity in the hemisphere contralateral to movement) remains somewhat intact in patients with a LD symptom profile, regardless of whether the movement is with the left or right.

Table 2
Linear mixed model analysis.

|                      | Beta ERD |         | PMBR |         |
|----------------------|----------|---------|------|---------|
|                      | F-value  | df      | p-Value |  F-value  | df      | p-Value |
| Effects              |          |         |       |          |         |       |
| Corrected model      | 5.433    | 7,74    | <0.001 | 1.926    | 7.74    | 0.077  |
| Affected side (LD, RD)| 11.119   | 1.74    | 0.001 | 8.464    | 1.74    | 0.005  |
| Hand moved (left, right) | 16.023   | 1.74    | <0.001 | 0.323    | 1.74    | 0.572  |
| Hemisphere (contra, ipsi) | 6.491    | 1.74    | 0.013 | 0.687    | 1.74    | 0.410  |
| Interactions         |          |         |       |          |         |       |
| Affected side × hand | 1.071    | 1.74    | 0.304 | 0.070    | 1.74    | 0.792  |
| Affected side × hemisphere | 0.067   | 1.74    | 0.796 | 0.241    | 1.74    | 0.625  |
| Hand × hemisphere    | 1.723    | 1.74    | 0.193 | 1.660    | 1.74    | 0.202  |
| Affected side × hand × hemisphere | 0.288 | 1.74    | 0.593 | 3.815    | 1.74    | 0.055  |

⁎Boldface denotes significance (p < 0.05).
Contra = contralateral to movement; ipsi = ipsilateral to movement.
hand. On the contrary, patients who exhibit a RD profile show less lateralized (i.e., more aberrant) beta ERD responses during right hand movements compared to LD patients. This, coupled with the overall reduced beta ERD amplitude during both left and right movements and in both hemispheres in these patients, suggests a greater impact of RD symptomatology on overall physiology throughout the entire motor network, with particularly severe aberrations for the right hand, which is in line with prior behavioral and metabolic data.

In sum, our study was the first to directly compare the laterality of motor-related beta oscillatory responses with symptom asymmetry in patients with PD whose symptoms were either LD or RD. Patients who had LD symptomatology had significantly greater beta ERD amplitude in the left primary motor cortex during right-hand movements compared to patients with RD symptomatology. Further, despite differences in overall beta power between LD and RD patients, we found a significant relationship between per-movement beta ERD lateralization and symptom asymmetry across groups in the right-hand, such that the more LD the symptoms, the more LD the beta ERD response. Future work should aim to elucidate the underlying cause of behavioral and neurophysiological differences between patients with LD and RD symptom profiles. Further, recent studies have identified several other Parkinson’s subtypes, based on motor subtypes, movement complications, etc. (Thenganatt and Jankovic, 2014), and the neurophysiology of these subtypes should also be the focus of future work. Thus, the complex interactions between Parkinson’s subtype, side of disease onset, and physiology remain to be discovered and are likely critical. Nonetheless, this study highlights the importance of taking patient symptom heterogeneity into consideration in research and the clinic, and suggests that future clinical and translational research studies should strongly consider dividing patients with PD into LD and RD subgroups. This study also provides preliminary evidence of the neurophysiological basis of preferential behavioral outcomes of LD patients compared to RD patients. Future studies should evaluate potential treatment differences among LD and RD patients, and consider monitoring the course of disease progression in separate LD and RD subgroups.

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References

Abe, K., Terakawa, H., Takanashi, M., Watanabe, Y., Tanaka, H., Fujita, N., Hirakubi, N., Yanagihara, T., 2000. Proton magnetic resonance spectroscopy of patients with Parkinsonism. Brain Res. Bull. 52, 589–595.
Alegre, M., Gurtubay, I.G., Labarga, A., Iriarte, J., Valencia, M., Artieda, J., 2004. Frontal and central oscillatory changes related to different aspects of the motor process: a study in go/no-go paradigms. Exp. Brain Res. 159, 14–22.
Alegre, M., Alvarez-Gerrirko, I., Valencia, M., Iriarte, J., Artieda, J., 2008. Oscillatory changes related to the forced termination of a movement. Clin. Neurophysiol. 119, 290–300.
Baumann, C.R., Held, U., Vallo, P.O., Wienecke, M., Waldvogel, D., 2014. Body side and predominant motor features at the onset of Parkinson’s disease are linked to motor and nonmotor progression. Mov. Disord. 29, 207–213.
Bohnen, N.J., Albin, R.L., Koepp, R.A., Wernette, K.A., kilburn, M.R., Minoshima, S., Frey, K.A., 2006. Positron emission tomography of monomeric vesicular binding in aging and Parkinson disease. J. Cereb. Blood Flow Metab. 26, 1198–1212.
Brown, P., 2007. Abnormal oscillatory synchronisation in the motor system leads to impaired movement. Curr. Opin. Neurobiol. 17, 655–664.
Cassidy, M., Mazzone, P., Oliviero, A., Insola, A., Tonali, P., Di Lazzaro, V., Brown, P., 2002. Movement-related changes in synchronisation in the human basal ganglia. Brain 125, 1233–1246.
Choe, B.Y., Park, J.W., Lee, K.S., Son, B.C., Kim, M.C., Kim, S.B., Suh, T.S., Lee, H.K., Shin, K.S., 1998. Neuronal laterality in Parkinson’s disease with unilateral symptom by in vivo 1H magnetic resonance spectroscopy. Invest. Radiol. 33, 450–455.
Djaldetti, R., Ziv, I., Melamed, E., 2006. The mystery of motor asymmetry in Parkinson’s disease. Lancet Neurol. 5, 796–802.
Doyle, L.M., Varrow, K., Brown, R., 2005. Lateralization of event-related beta desynchronization in the EEG during pre-cued reaction time tasks. Clin. Neurophysiol. 116, 1878–1889.
Eidelberg, D., Moeller, J.R., Dhawan, V., Säidis, J.J., Ginos, J.Z., Strother, S.C., Cederbaum, J., Greene, P., Fahn, S., Rottenberg, D.A., 1990. The metabolic anatomy of Parkinson’s disease: complementary [18F]fluorodopa and [18F]fluorodeoxyglucose positron emission tomographic studies. Mov. Disord. 5, 203–213.
Ernst, M.D., 2004. Permutation methods: a basis for exact inference. Stat. Sci. 19, 676–685.
Frazzitta, G., Ferrazzoli, D., Maestri, R., Rovescala, R., Guaglio, G., Bera, R., Volpe, D., Pezzoli, G., 2015. Differences in muscle strength in parkinsonian patients affected on the right and left side. PLoS One 10, e0121251.
Fry, A., Mullinger, K.J., O’Neill, G.C., Barratt, E.L., Morris, P.G., Bauer, M., Folland, J.P., Brookes, M.I., 2016. Modulation of post-movement beta rebound bycontraforce and rate of force development. Hum. Mov. Sci. 37, 2493–2511.
Gaetz, W., Macdonald, M., Cheyne, D., Snaed, O.C., 2010. Neuronal magnetic imaging of movement-related cortical oscillations in children and adults: age predicts post-movement beta rebound. Neuroimage 51, 792–807.
Goetz, C.G., Fahn, S., Martinez-Martin, P., Poewe, W., Sampaio, C., Stebbins, G.T., Stern, M.B., Tilley, B.C., Dodel, R., Dubois, B., Holloway, R., Jankovic, J., Kulisevsky, J., Lang, A.E., Lees, A., Leurgans, S., LeWitt, P.A., Nyenhuis, D., Olanow, C.W., Rascol, O., Schrag, A., Teresi, J.A., Van Hillen, J.J., LaPelle, N., 2007. Movement Disorder Society-sponsored revision of the Unified Parkinson’s Disease Rating Scale (MDS-UPDRS): progress, format, and clinimetric testing plan. Mov. Disord. 22, 41–47.
Grafton, S.T., Oostenveld, R., Jensen, O., Medendorp, W.P., Pfurtscheller, G., 2014. Competitive interactions in sensorimotor cortex: oscillations express separation between alternative movement targets. J. Neurophysiol. 112, 224–232.
Gross, J., Kujala, J., Hamalainen, M., Timme, M., Schnitzler, A., Salminen, R., 2001. Dynamic imaging of coherent sources: studying neural interactions in the human brain. U. S. A]–Proc. Natl. Acad. Sci. U. S. A 98, 694–699.
Haaxma, C.A., Helmich, R.C., Born, G.F., Kappelle, A.C., Horstink, M.W., Bloem, B.R., 2010. Side of symptom onset affects motor dysfunction in Parkinson’s disease. Neurosci- ence 170, 1282–1285.
Hall, S.D., Prokis, E.J., McAllister, C.J., Ronqvist, K.C., Williams, A.C., Yamawaki, N., Witton, C., Woodhall, G.L., Stanford, I.M., 2014. GABA-mediated changes in inter-hemispheric beta frequency activity in early-stage Parkinson’s disease. Neuroscience 281, 68–76.
Hammond, C., Bergman, H., Brown, P., 2007. Pathological synchronization in Parkinson’s disease: networks, models and treatments. Trends Neurosci. 30, 357–364.

Heinrichs-Graham, E., Wilson, T.W., 2015. Coding complexity in the human motor circuit. Hum. Brain. Map. 36, 5155–5167.

Heinrichs-Graham, E., Wilson, T.W., 2016. Is an absolute level of cortical beta suppression required for proper movement? Magnetoencephalographic evidence from healthy aging. NeuroImage 134, 514–521.

Heinrichs-Graham, E., Kurz, M.J., Becker, K.M., Santamaria, P.M., Gendelman, H.E., Wilson, T.W., 2014a. Hypersynchrony despite pathologically reduced beta oscillations in patients with Parkinson’s disease: a pharmaco-magnetoencephalography study. J Neurophysiol. 112, 1739–1747.

Heinrichs-Graham, E., Wilson, T.W., Santamaria, P.M., Heitoff, S.K., Torres-Russotto, D., Hutter-Saunders, J.A., Estes, K.A., Meza, J.L., Mosley, R.L., Gendelman, H.E., 2014b. Neuroneural evidence of abnormal movement-related beta desynchronization in Parkinson’s disease. Cereb. Cortex 24, 2669–2678.

Heinrichs-Graham, E., Arpin, D.J., Wilson, T.W., 2016. Cue-related temporal factors modulate movement-related beta oscillatory activity in the human motor circuit. J. Cogn. Neurosci. 28, 1039–1051.

Hillebrand, A., Singh, K.D., Holliday, J.E., Furlong, P.L., Barnes, C.R., 2005. A new approach to neuroimaging with magnetoencephalography. Hum. Brain. Map. 25, 199–211.

Hoehn, M.M., Yahr, M.D., 2001. Parkinsonism: onset, progression, and mortality. 1967.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Jankovic, J., 2008. Parkinson’s disease: clinical features and diagnosis. J. Neurol. Neurosurg. Psychiatry 55, 73–1289.

Jiang, J., 2007. Linear and Generalized Linear Mixed Models and Their Applications. 1 ed. Heinrichs-Graham, E., Wilson, T.W., 2016. Is an absolute level of cortical beta suppression required for proper movement? Magnetoencephalographic evidence from healthy aging. NeuroImage 134, 514–521.

Jankovic, J., 2008. Parkinson’s disease: clinical features and diagnosis. J. Neurol. Neurosurg. Psychiatry 55, 73–1289.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Jiang, J., 2007. Linear and Generalized Linear Mixed Models and Their Applications. 1 ed. Springer-Verlag, New York.

Jurgiewicz, M.T., Gaetz, W.C., Bostan, A.C., Cheyne, D., 2006. Post-movement beta rebound or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Liu, S.C., Lin, K.J., Hsiao, I.T., Hisieh, C.J., Lin, W.Y., Yu, C.S., Wey, S.P., Yen, T.C., Kung, M.P., Weng, Y.H., 2014. In vivo detection of monoaminergic degeneration in early Parkinson’s disease by (18)F-9-fluorophenyl-(+)-dihydrotetrahydroazepine PET. J. Nucl. Med. 55, 73–79.

Jang, J., 2007. Linear and Generalized Linear Mixed Models and Their Applications. 1 ed. Springer-Verlag, New York.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Liu, S., Brown, P., 2014. The functional role of beta oscillations in Parkinson’s disease. Cereb. Cortex 24, 2669–2678.

Jankovic, J., 2008. Parkinson’s disease: clinical features and diagnosis. J. Neurol. Neurosurg. Psychiatry 55, 73–1289.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Lee, C.S., Schulzer, M., Mak, E., Hammerstad, J.P., Calne, S., Calne, D.B., 1995. Patterns of asymmetry do not change over the course of idiopathic Parkinsonism: implications for pathogenesis. Neurology 45, 435–439.

Lin, S.C., Lin, K.J., Hsiang, I.T., Hisieh, C.J., Lin, W.Y., Yu, C.S., Wey, S.P., Yen, T.C., Kung, M.P., Weng, Y.H., 2014. In vivo detection of monoaminergic degeneration in early Parkinson’s disease by (18)F-9-fluorophenyl-(+)-dihydrotetrahydroazepine PET. J. Nucl. Med. 55, 73–79.

Jang, J., 2007. Linear and Generalized Linear Mixed Models and Their Applications. 1 ed. Springer-Verlag, New York.

Kempster, P.A., Gibb, W.R., Stern, G.M., Lees, A.J., 1989. Asymmetry of substantia nigra or EEG into components. Med. Biol. Eng. Comput. 35, 135–140.

Liu, S., Brown, P., 2014. The functional role of beta oscillations in Parkinson’s disease. Parkinsonism Relat. Disord. 20 (Suppl. 1), 544–548.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Lee, C.S., Schulzer, M., Mak, E., Hammerstad, J.P., Calne, S., Calne, D.B., 1995. Patterns of asymmetry do not change over the course of idiopathic Parkinsonism: implications for pathogenesis. Neurology 45, 435–439.

Lin, S.C., Lin, K.J., Hsiang, I.T., Hisieh, C.J., Lin, W.Y., Yu, C.S., Wey, S.P., Yen, T.C., Kung, M.P., Weng, Y.H., 2014. In vivo detection of monoaminergic degeneration in early Parkinson’s disease by (18)F-9-fluorophenyl-(+)-dihydrotetrahydroazepine PET. J. Nucl. Med. 55, 73–79.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.

Litvak, V., Jha, A., Eusebio, A., Ostenveld, R., Folyne, T., Limousin, P., Zrinzo, L., Hariz, M.I., Friston, K., Brown, P., 2011. Resting oscillatory cortico-subthalamic connectivity in patients with Parkinson’s disease. Brain 134, 359–374.