Monolayer MoS$_2$-Based Flexible and Highly Sensitive Pressure Sensor with Wide Sensing Range

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Abstract: Flexible pressure sensors play an important role in flexible robotics, human-machine interaction (HMI), and human physiological information. However, most of the reported flexible pressure sensors suffer from a highly nonlinear response and a significant decrease in sensitivity at high pressures. Herein, we propose a flexible novel iontronic pressure sensor based on monolayer molybdenum disulfide (MoS$_2$). Based on the unique structure and the excellent mechanical properties as well as the large intercalation capacitance of MoS$_2$, the prepared sensor holds an ultra-high sensitivity ($S_{\text{max}} = 89.75$ kPa$^{-1}$) and a wide sensing range (722.2 kPa). Further, the response time and relaxation time of the flexible sensor are only 3 ms, respectively, indicating that the device can respond to external pressure rapidly. In addition, it shows long-term cycling stability (over 5000 cycles with almost no degradation) at a high pressure of 138.9 kPa. Finally, it is demonstrated that the sensor can be used in physiological information monitoring and flexible robotics. It is anticipated that our prepared sensor provide a reliable approach to advance the theory and practicality of the flexible sensor electronics.

Keywords: flexible electronics; flexible sensor; wearable sensor; iontronic pressure sensor; MoS$_2$

1. Introduction

Flexible pressure sensors are widely used in human-machine interaction (HMI) [1–3], electronic skin (E-Skin) [4–6], and human health monitoring [7–11]. In particular, capacitive pressure sensors have attracted a broad attention with their merits of low power, excellent stability and fast response time. But building flexible capacitive pressure sensors with high sensitivity and wide sensing range has been a challenge when considered the sensitivity of conventional capacitive pressure sensors is typically relatively low.

Iontronic pressure sensors have recently attracted a lot of attention [12–17]. This type of interfacial capacitive sensor based on electrical double layer (EDL) capacitance has the advantages of ultra-high capacitance ($\mu$F cm$^{-2}$) and high signal-to-noise ratio (SNR), which are not available with conventional flat plate capacitive sensor. The EDL performance depends on many items, among which the electrode materials play a most important role. Currently reported sensitive materials for preparing iontronic pressure sensor is categorized into metal-based electrode materials [18,19], carbon-based materials [7], metal oxide indium tin oxide (ITO) [20], and MXene [21]. Metal electrodes typically exhibit smaller specific surface area and reduced EDL capacitance. In the case of carbon materials,
the electrodes are thicker, mechanically prone to fracture and have longer ion transport paths, while MXene faces problems such as oxidation. Therefore, the deep research on new materials for iontronic pressure sensor and the further study of their sensing mechanisms are important for the development of flexible iontronic sensors.

As a new two-dimensional material, molybdenum disulfide (MoS\(_2\)) have attracted a lot of attention in recent years, and it has been widely used in supercapacitors, micro-electronic devices, and batteries because of its rich elemental composition, wide band gap (1.29–1.90 eV), high electron mobility, excellent thermal properties and good mechanical properties [22–24]. Therefore the MoS\(_2\) has the potential to be used as an electrode material in iontronic pressure sensors. However, the study on the monolayer MoS\(_2\)-based flexible iontronic pressure sensor are rarely reported.

Therefore, in order to solve the problem of sensitivity and sensing range balance of the flexible pressure sensor, we propose a novel iontronic pressure sensor based on MoS\(_2\) monolayer. The monolayer MoS\(_2\)/gold composite electrode was obtained by wet transfer strategy. And the iontronic pressure sensor was assembled by the composite electrode and microstructural ionic film. Thanks to the excellent mechanical-electrical properties of MoS\(_2\) and unique layered structure, the prepared sensor shows an unprecedented ultra-high sensitivity (\(S_{\text{max}} = 89.75 \text{ kPa}^{-1}, S_{\text{min}} = 10.24 \text{ kPa}^{-1}\)) and a wide sensing range (722.2 kPa). The response time and relaxation time of the sensor sensor are both 3 ms, respectively. Moreover, the possible sensing mechanism of the sensor is proposed. Finally, the application of this novel iontronic pressure sensor is carefully demonstrated.

2. Materials and Methods

2.1. Preparation of MoS\(_2\)/Au Composite Electrode

The Au/PI (polyimide) was prepared by magnetron sputtering. A thin 100 nm gold layer was sputtered on the cleaned PI film. A monolayer MoS\(_2\) grew on the Si/SiO\(_2\) (Silicon/Silicon dioxide) wafer (SiO\(_2\) layer thickness, 300 nm) by chemical vapor deposition (CVD) method. A PMMA (polymethyl methacrylate) film was covered on the MoS\(_2\) layer as a supporting protective layer by spin-coating method (3000 r min\(^{-1}\), 10 s), and dried completely at 100 °C for 10 min. Then, the samples were placed in a KOH (potassium hydroxide) solution (1 mol L\(^{-1}\)) with a heating temperature of 90 °C to etch the growth substrate to separate the PMMA/MoS\(_2\) from the Si/SiO\(_2\) substrate. After the sample was completely separated from the substrate, PMMA/MoS\(_2\) was transferred to deionized water and soaked several times to remove the residue KOH solution, and then PMMA/MoS\(_2\) was transferred to the Au/PI electrode. Finally, the PMMA film was removed using acetone, and the electrode was cleaned with isopropyl alcohol and deionized water several times to remove the residual acetone.

2.2. Preparation of PVA/H\(_3\)PO\(_4\) Film with Pyramid Microstructure

1 g of Polyvinyl Alcohol (PVA) was mixed with deionized water (10 mL) under serious stirring at 85 °C for one hour until completely dissolved to a transparent state. Then the 85% H\(_3\)PO\(_4\) solution (2 mL) was added to the prepared PVA solution drop by drop, and then stirring continued for half an hour at 90 °C to make the uniform dispersion. Finally, the prepared gel electrolyte was evenly coated on the mask template with pyramidal microstructure and the thickness was controlled at 10 μm by spin coating. After the film was dried at 60 °C for one hour, the film can be peeled off from the substrate.

2.3. Fabrication of Flexible Pressure Sensor

The prepared gold electrode with a monolayer MoS\(_2\) on PI substrate, the poly (ethylene terephthalate) PET spacer layer, the PVA/H\(_3\)PO\(_4\) ionic film with upside-down pyramid microstructure are stacked in a “sandwich” configuration PET with a thickness of about 100 μm was employed as the spacer, and finally 3M tape was used to ensure the fully integrated encapsulation of the device.
2.4. Material and Structural Characterization

Field emission scanning electron microscopy (FESEM, Quanta 450, 20 kV) were used to characterize the structure and morphology information. Raman spectroscopy were measured by a Renishaw inVia Raman spectrometer (Renishaw, Britain, UK). For each test on MoS$_2$, three samples were prepared and five points on each sample were measured.

2.5. Electrical and Mechanical Characterization

For the electromechanical characterization, the variable capacitance can be recorded by LCR impedance analyzer (Tonghui, TH 2827A, Changzhou, China) and IM3536 LCR meter (HIOKI, Taiwan, China) linkage test. The CV curves also were shown on the electrochemical working station (CHI 760E, Chen Hua, Shanghai, China) under the applied pressure. For featuring cyclic stability, the device was tested on a mechanical testing machine (Zhi Qu, 990B, Dongguan, China) with the pulling speed of 5 mm min$^{-1}$.

3. Results and Discussion

MoS$_2$ possess excellent intercalating pseudocapacitive and EDL properties for charge storage. And it has been shown that MoS$_2$ has faster electron transfer capability than oxide and higher theoretical specific capacitance than graphene when used as an electrode material. Therefore, in this study, a monolayer MoS$_2$ is introduced as the electrode to improve the capacitance and further boost the sensitivity of the sensor. The monolayer MoS$_2$ was transferred by wet transfer method (Figure 1) on an Au/PI film. The assembled device is shown in Figure 1b. The size of the prepared sensor is $1 \times 1$ cm$^2$, which is small compared with a coin, demonstrating its portable and flexible feature. Noted that the microstructural ionic film was beneficial to further improve the sensitivity of the sensor, which has been demonstrated by previous reports [25].

![Figure 1](image1.png)

**Figure 1.** Preparation and schematic diagram of iontronic pressure sensor. (a) Wet transfer process of MoS$_2$ monolayer. (b) Digital optical image and flexible feature of iontronic pressure sensor and the corresponding diagram layout of each layer in the sensor.

The monolayer MoS$_2$ was transferred onto the Au/PI electrode by wet transfer method [26], and the optical microscope of the electrode is shown in Figure 2a. From which it can be observed that the large and continuous monolayer MoS$_2$ on the Au/PI film showed good integrity and only a very few cracks existed due to etching when the support layer was removed during the transfer process. The Raman results further certified the MoS$_2$ property. The number of layers of the sample can be determined according to the wave number difference between E$^{1\text{g}}_{2\text{g}}$ and A$_{1\text{g}}$, from Raman spectra of monolayer MoS$_2$. 
Wave number difference of bulk material is 26 cm$^{-1}$, while the wave number difference between A$_{1g}$ and E$^{1}_{2g}$ in Figure 2b is 19 cm$^{-1}$. Hence, the preparative sample of MoS$_2$ can be regarded as monolayer with the thickness of 6.15 Å [27,28]. Further, SEM of the monolayer MoS$_2$ before and after the transfer was performed in Figure 2c,d. It can be observed that the monolayer MoS$_2$ on the Si/SiO$_2$ substrate is large area continuous growth without a clear defect. Also, as shown in Figure 2d, the monolayer MoS$_2$ can still be observed as a continuous boundary which is similar to that before transfer to the target substrate by the wet transfer method. This further indicates that the monolayer MoS$_2$ obtained by the wet transfer method has a high integrity with few significant cracks, which lays the foundation for the preparation of the sensor electrode. Finally, SEM of the monolayer MoS$_2$ after 5000 cycle test was performed in Figure 2e,f.

![Figure 2](image_url)

Figure 2. Characterization of the sensor electrodes for flexible sensors. Scanning electron microscopy (SEM) images of monolayer MoS$_2$. (a) Optical image of the monolayer MoS$_2$ on Au/PI film. (b) Raman data of the monolayer MoS$_2$. (c,d) SEM of the monolayer MoS$_2$ before and after transfer process. (e,f) SEM image after 5000 cycle stability test.

The digital optical image of the ionic membrane is shown in Figure 3a, which exhibits excellent flexibility. The microstructure of the inverted pyramid is clearly visible (Figure 3b).
The prepared PVA/H₃PO₄ ionic membrane was further characterized by SEM, as shown in Figure 3c. It can be clearly seen that the microstructure of the prepared ionic membrane is well established, exhibiting an inverted pyramidal structure with each size of about 100 µm. The cross-sectional structure of the ionic membrane is shown in Figure 3d, which shows that the membrane has a distinct pyramidal protrusion structure with a height of about 70 µm. The microstructure has been demonstrated to significantly improve the sensitivity of the flexible sensor. When the microstructure is compressed, due to the initial mechanically non-stationary state, it is easy to deform thus causing a rapid increase in the contact area between the electrode and the ionic membrane, thus increasing the capacitance and sensitivity of the sensor.

![Figure 3a](image1.png)

![Figure 3b](image2.png)

![Figure 3c](image3.png)

![Figure 3d](image4.png)

**Figure 3.** Characterization of the ionic film for flexible sensors. (a) Low and (b) high magnification of the optical image of the ionic film. (c) SEM image of the ionic film. (d) Cross-sectional view of the ionic film.

The performance of the sensor is investigated as shown in Figure 4. The maximum sensitivity ($S_{\text{max}}$) of the MoS₂-based iontronic pressure sensor is 89.75 kPa$^{-1}$ up to 55.6 kPa, and the minimum sensitivity ($S_{\text{min}}$) is 10.24 kPa$^{-1}$ in the range of 55.6 kPa to 722.2 kPa, which is superior to our previous work and other works [29–34]. Also, an iontronic pressure sensor with the same structure but without the MoS₂ layer was prepared as a control group. The results showed that its sensitivity was 0.031 kPa$^{-1}$, which demonstrated the important role of the MoS₂ layer. The increased capacitance is derived from the unique layer structure, huge specific surface area and pseudocapacitance characteristics.
138.9 kPa, 555.6 kPa, and 722.2 kPa respectively, as shown in Figure 4b. The signal of the sensor is constant for each test, and can be rapidly recovered after the force is removed. The stable and proportional electrical signal output at different pressures indicates that the sensor can maintain high stability with small signal drift. To evaluate the dynamic response speed of the pressure sensor, a weight of 1 g (equivalent pressure ~0.01 N) was gently placed on the pressure sensor followed by a quick release revealing a 3 ms response time and relaxation time in Figure 4c. This indicates that the prepared sensor can respond quickly to the applied external stimulus and has a good dynamic response. Even after continuous pressure of 138.9 kPa for 5000 cycles, as shown in Figure 4d, the sensor still maintained a stable signal output with no significant attenuation, demonstrating its long-term use application. Small cracks were found on the surface of monolayer MoS$_2$ but they did not affect final signal response in Figure 4d.

Figure 4. The performance of the flexible sensor. (a) Capacitance variation of the sensor under various pressure. (b) Continuous pressure test of the sensor. (c) Response and relaxation time of the flexible sensor. (d) Durability test of the sensor under applied pressure of 138.9 kPa for 5000 cycles.

The stability of the sensor subject to the same pressure is also one of the important factors. The sensor was tested under four different continuously pressure of 27.8 kPa, 138.9 kPa, 555.6 kPa, and 722.2 kPa respectively, as shown in Figure 4b. The signal of the sensor is constant for each test, and can be rapidly recovered after the force is removed. The stable and proportional electrical signal output at different pressures indicates that the sensor can maintain high stability with small signal drift. To evaluate the dynamic response speed of the pressure sensor, a weight of 1 g (equivalent pressure ~0.01 N) was gently placed on the pressure sensor followed by a quick release revealing a 3 ms response time and relaxation time in Figure 4c. This indicates that the prepared sensor can respond quickly to the applied external stimulus and has a good dynamic response. Even after continuous pressure of 138.9 kPa for 5000 cycles, as shown in Figure 4d, the sensor still maintained a stable signal output with no significant attenuation, demonstrating its long-term use application. Small cracks were found on the surface of monolayer MoS$_2$ but they did not affect final signal response in Figure 4d.

Also, the sensor was further tested at different frequencies (0.1, 0.2 and 1 Hz) at the same pressure (138.9 kPa). As shown in Figure 5a, the sensor maintained a stable
signal at various frequency, demonstrating that the sensor’s excellent dynamic response. Importantly, the CV curve of the sensor under 722.2 kPa was investigated to find the deep sensing mechanism. As shown in Figure 5b, the CV curve is not ideally rectangular, and shows a small peak in redox, which is further evidence of the pseudo-capacitance effect as described above.

Based on the above, the superior performance of the sensor has been demonstrated and its sensitivity mechanism was revealed as shown in Figure 6. In this study, in addition to improving the sensitivity by MoS$_2$ layer, a spacer layer is also introduced between the ionic film and the electrode (Figure 6a). Initially, the capacitance is extremely small due to the presence of the spacer layer. When the sensor is subjected to pressure, the upper electrodes layer was bent due to stress and the distance between the two electrodes becomes narrow, resulting in a larger capacitance ($C_{PE}$, Figure 6b). Further, when the force continues to be applied, the electrodes began contact with the ionic membrane ($C_{EDL1}$), causing a rapid increase in EDL capacitance. With further increase in force, the contact area between the microstructure of the ionic membrane and the lower electrode further increases and the capacitance further becomes larger ($C_{EDL2}$), leading to higher capacitance changes. In addition, it is obvious from the simulation that the deformation of the microstructure is mainly concentrated in the middle part of the microstructure rather than the tip of the structure, which may be due to the unique shape of the microstructure. It is also confirmed that the microstructure can improve the capacitance of the sensor.

**Figure 5.** (a) Capacitance variation of the sensor under various frequencies. (b) CV curve of the sensor at a scan rate of 50 mV s$^{-1}$.

**Figure 6.** Schematic illustration of the working mechanism of the sensor. (a) Sensing mechanism of the iontronic pressure sensor and the stress concentration of the microstructure. (b) Corresponding capacitance variation of the sensor.
To investigate the application of the iontronic pressure sensor, the sensor was mounted on the human body to detect the movement. As shown in Figure 7a, with the rapid change of the finger to a small angle, the signal output of the sensor is consistent each time, indicating that the sensor can accurately recognize the bending of the finger. Subsequently, with a rapid change of the finger to a large angle (about 90°), the signal output amplitude increases significantly compared to the previous small angle change, suggesting that the sensor can accurately recognize different angle changes of the finger. In addition to the finger, the sensor can also detect wrist and arm bending as well as eye blinking (Figure 7b–d). These above demonstrated that the sensor has the ability to detect human motion and has important applications in the health rehabilitation of the human body. To simulate the scene of gas leak monitoring, an aurilave was used to imitate airflow. Under subtle signals, the sensor response was captured. Figure 7e has shown the variation of capacitance over time, which demonstrated that stable output can also be achieved for subtle signals. As summarized in Figure 7f [35–43], our Monolayer MoS$_2$-based iontronic pressure sensor shows an incomparably high sensitivity and an ultrabroad work range of pressure, out-performing existing capacitance pressure sensor.

Figure 6. Schematic illustration of the working mechanism of the sensor. (a) Sensing mechanism of the iontronic pressure sensor and the stress concentration of the microstructure. (b) Corresponding capacitance variation of the sensor.

Figure 7. Practical application of the flexible iontronic sensor for motion monitoring. Capacitance variations of the sensor during (a) finger (b) wrist (c) arm bending and (d) eye blinking. (e) Capacitance response output of gas leak monitoring, and the image is shown in the inset. (f) Comparison of the sensitivity of our pressure sensor with existing capacitive sensors.
Further, we directly mounted the flexible sensor on the flexible manipulator and use the manipulator to grasp objects of different weights. In this study, pears and apples of different weights but similar shapes for comparison. As shown in Figure 8, the capacitance change trend of both is the similar, but the magnitude is different, which is due to the different magnitude of force applied by the manipulator when grasping two different weight objects. This successfully demonstrates that the prepared sensor has the ability to recognize the weight of the target and can be used as a tactile sensor to fix on the flexible manipulator to recognize the mass of the object.

Figure 8. Application of the sensor on flexible robotics. (a) The process to grasp and release apple; (b) Corresponding steps for the soft manipulator to grasp and release the apple and pear sample.

4. Conclusions

In summary, a highly sensitive iontronic pressure sensor based on EDL sensing mechanism was designed and prepared. The electrodes based on a monolayer MoS$_2$ were successfully prepared by the wet transfer method, and the PVA/H$_3$PO$_4$ ionic membrane with inverted pyramid microstructure was beneficial to enhancing the sensitivity. The pressure sensor showed a high sensitivity of $89.75 \text{kPa}^{-1}$ in the sensing range of $722.2 \text{kPa}$. Additionally, the sensor exhibited a short response time and relaxation time. Through analysis, the unique structure-induced high capacitance, the rationally designed structure such as the microstructural ionic film and device configuration are all beneficial to enhancing the sensitivity and sensing range. Finally, it is verified that the sensor has a great potential for motion detection and flexible robotics applications. Our sensor design makes a novel strategy for flexible sensor electronics and will inspire more committee focus on 2D materials-based sensor.

The next research should focus on the following items.

Firstly, the effect of different layers of MoS$_2$ on the performance of the sensor and the mechanism of the effect should be investigated.

Secondly, the sensors should be further miniaturized to prepare higher integrated sensors such as the sensor arrays with a high sensitivity to achieve a large-scale application.

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