The statistical mechanics of complex signaling networks: nerve growth factor signaling

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Abstract
The inherent complexity of cellular signaling networks and their importance to a wide range of cellular functions necessitates the development of modeling methods that can be applied toward making predictions and highlighting the appropriate experiments to test our understanding of how these systems are designed and function. We use methods of statistical mechanics to extract useful predictions for complex cellular signaling networks. A key difficulty with signaling models is that, while significant effort is being made to experimentally measure the rate constants for individual steps in these networks, many of the parameters required to describe their behavior remain unknown or at best represent estimates. To establish the usefulness of our approach, we have applied our methods toward modeling the nerve growth factor (NGF)-induced differentiation of neuronal cells. In particular, we study the actions of NGF and mitogenic epidermal growth factor (EGF) in rat pheochromocytoma (PC12) cells. Through a network of intermediate signaling proteins, each of these growth factors stimulates extracellular regulated kinase (Erk) phosphorylation with distinct dynamical profiles. Using our modeling approach, we are able to predict the influence of specific signaling modules in determining the integrated cellular response to the two growth factors. Our methods also raise some interesting insights into the design and possible evolution of cellular systems, highlighting an inherent property of these systems that we call ‘sloppiness.’

This article has associated online supplementary data files
(Some figures in this article are in colour only in the electronic version)

1. Introduction
Recent experimental data point to the complexity underlying eukaryotic signal transduction pathways. Pathways once thought to be linear are now known to be highly branched, and
modules formerly thought to operate independently participate in a substantial degree of crosstalk (Schlessinger 2000, Hunter 2000). It is this complexity that has motivated attempts to use quantitative mathematical models to better understand the behavior of cellular signaling networks. Models using nonlinear differential equations have often been used in the attempt to understand biological regulation in eukaryotes and have recently been applied to the cell cycle in yeast (Chen et al 2000), circadian rhythms (Goldbeter 1995), establishment of segment polarity in flies (von Dassow et al 2000), and transport dynamics of the small GTPase Ran (Smith et al 2002). Currently, a consortium called the Alliance for Cellular Signaling is embarking on a vastly more ambitious project, coupling experiment and computation, to understand signaling in a model macrophage cell line (Principle investigators and scientists of the Alliance for Cellular Signaling 2002).

Modeling of complex signaling modules presents three key challenges. (1) Any model based on the equations of chemical kinetics will likely contain a large number of parameters whose values will not have been determined experimentally (Bailey 2001). Even in cases where a specific measurement has been made in vitro (i.e. a binding constant or turnover rate), the value obtained may differ substantially from what would have been measured in cells if such a measurement were possible (Minton 2001). Recent success has been achieved in facilitating the extraction of transcriptional rates from experimental measurements of promoter activity (Ronen et al 2002), but the problem remains extremely difficult for complex cellular signaling systems comprising large numbers of protein–protein interactions. (2) Kinetic models tend to be incomplete because they often ignore many protein interactions in the hopes of capturing a few essential ones. Thus, one ends up dealing with a ‘renormalized’ model in which existing parameters absorb the effects of all the neglected parameters in the ‘true’ model (Golikeri and Luss 1974). (3) Additional difficulties arise from the fact that novel interacting proteins and new interactions for well-known players continue to be discovered (Vojtek and Der 1998), so one must have a flexible modeling methodology that can easily incorporate new information and data. These three challenges make the modeling of complex cellular signaling networks inherently difficult.

We believe that modeling these important biological systems cannot wait until all the rates are reliably measured, or even until all the various players and interactions are discovered. Indeed, the most important role of modeling is to identify missing pieces of the puzzle. It is as useful to falsify models—identifying which features of the observed behavior cannot be explained by the experimentalists current interaction network—as it is to successfully reproduce known results. We choose the straightforward (but not standard) approach of directly simulating the differential equations given by the reactions in our network. There are a variety of other approaches to modeling these networks. Systems models (Tyson et al 2001) typically reduce the large number of equations via a series of biologically-motivated approximations to a few key reactions: implementing these approximations demands deep insight that is often not available for complex cellular signaling systems. Boolean models are faster to simulate, but tend to be farther removed from the biology, and can be misleading even in some simple cases (Guet et al 2002). We also have chosen not to incorporate stochastic effects due to number fluctuations (Arkin et al 1998), nor are we exploring the validity of the experimentally presumed Michaelis–Menten reactions. This is not because we believe that stochastic effects are negligible nor that Michaelis–Menten assumptions are free of limitations, but rather we are testing the experimentalist’s assumptions that stochastic effects are not central and that the traditional saturable reaction forms are likely to be close to the real behavior in our particular system.

Our choice of simulating the full set of rate equations, and our desire to extract falsifiable predictions without prior knowledge of a large number of rate constants and other parameters, demand that we develop new modeling tools (Bailey 2001). In this study we apply ideas from statistical mechanics (Brown and Sethna 2003, Metropolis et al 1953, Newman and Barkema 1999, Hastings 1970, Battogtokh et al 2002) to extract predictions from a model for a regulatory signaling network important for the differentiation of a neuronal cell line. We show that this approach can make useful biological predictions even in the face of indeterminacy of parameters and of network topology. An underlying feature of the approach involves the use of Monte Carlo methods in Bayesian sampling of model spaces (Robert and Casella 1999, Hastings 1970); such a sampling method was recently applied to a small transcriptional network (Battogtokh et al 2002). Our implementation and notation is described in the ‘experimental section’, together with a brief discussion of its advantages and numerical details. We have chosen a relatively well-studied system—Erk activation in PC12 cells—as a test case for our analysis in order to demonstrate that our methods will have broad applicability for cellular signaling problems. We show that our approach can make useful predictions even in the face of underdetermined parameters and uncertainty with regard to network topology. However, perhaps most important, our methods highlight some interesting and previously unappreciated features that we believe are fundamentally inherent to complex cellular signaling systems.

2. Experimental section

2.1. Data fitting

A cost function such as that in (9) allows us to use automated parameter determination with the algorithm of our choice. Multiple metastable states are the norm rather than the exception in high-dimensional nonlinear systems such as those found in models of eukaryotic signal transduction. We use a simple procedure to discover different minima. Fixed-temperature annealing (Kirkpatrick et al 1983) is used to cross barriers between local minima, and selected parameter sets obtained via this process are quenched using a local method such as Levenberg–Marquardt (Marquardt 1963) or conjugate gradient (Fletcher 1987). For the PC12 cell network, we found
a few shallow minima separated by large flat regions. The minima showed qualitatively similar behavior but differed slightly in the quality of fit. All inferences from best fit parameters were performed using the best minimum found.

We note here that while cost minimization, Hessian matrix computation and our Monte Carlo (see below) all require many cost evaluations, the methods we employ are easily parallelizable, leading to great gains in computational efficiency. In addition, two of us show elsewhere (Brown and Sethna 2003) that if one is concerned primarily with the identity of the stiffest few eigenvectors, an approximate Hessian whose computational requirements scale only linearly (rather than quadratically) with the number of parameters is equally suitable.

The best fit parameters, Hessian (equation (4)), and Jacobian matrix (equation (8)) are all available online9.

2.2. Robustness calculations

The calculations whose results are displayed in figure 3 were obtained as follows. Assuming a quadratic cost space, we can write the expected change in cost given a change in the log of one parameter

\[ C(\Delta \log p_i) = C_0 + \frac{1}{2} H_{ii}(\Delta \log p_i)^2, \]

where \( H_{ii} \) is a diagonal element of the Hessian defined in (4) and \( C_0 \) is the value of the cost at the best fit parameter values. Here and elsewhere in this paper, all logarithms are to the base \( e \). We therefore define \( H_{ii}/2 \) as the inverse of the robustness of the model to a change in the \( i \)th parameter. Implicit in this definition is the set of network functions/outputs in which one is interested, since these form the constraining data set and exert their effect in \( H_{ii} \). For example, the robustness values calculated in figure 3(a) used our full experimental data set, containing 68 data points (time series for multiple protein activities in response to both growth factors), and those of figure 3(b) used only ten data points (the time series of Erk1/2 activation in response to both EGF and NGF). Also necessary is a scale on which to calibrate the robustness result; we deem a parameter robust if moving it by a factor of 2 causes the model probability (given by \( \exp(-C) \)) to decrease less than 1/e. In figure 3, this scale is indicated by a horizontal dashed line.

2.3. Ensembles

We associate the cost in (10) with the energy of a statistical mechanical system. The temperature \( T = 1 \) is set by comparing the form of the Boltzmann distribution to the probability of generating the data given the model (which in this case means providing a network diagram, a set of equations that govern the protein dynamics, and a set of values for all the parameters) if the errors in the data are normally distributed. Additionally, we use information about the shape of the cost basins near the minima via the second derivative matrix of the cost (the Hessian) to generate the moves in parameter space. At finite temperature, the \( B_k \) give an entropic contribution to the cost which can be determined analytically, and it is this free energy—cost plus entropy from the \( B_k \)—that we use in all thermal contexts (Brown and Sethna 2003). From the ensemble, a mean \( \langle [C(t)] \rangle \) and standard deviation \( \sigma(t) \) as a function of time are generated for each chemical concentration, given for the \( i \)th chemical by

\[ \langle [C_i(t)] \rangle = \frac{1}{N_E} \sum_{j=1}^{N_E} [C_i(p_j, t)], \]

\[ \sigma_i(t) = \left( \langle [C_i(p_j, t)]^2 \rangle - \langle [C_i(p_j, t)] \rangle^2 \right)^{1/2}, \]

where \( N_E \) is the number of samples in the ensemble.

We start all Monte Carlo runs at the best fit parameters, though it is not absolutely necessary to do so. We selected 704 independent parameter sets from over 15 000 sets initially generated by the Monte Carlo. We chose independent states by first calculating the correlation time \( \tau \) which we can obtain from the lagged cost–cost correlation \( \langle A(n) = \langle C(p_j) C(p_{ns}) \rangle \rangle \) function from a given Monte Carlo run. \( \tau \) was defined as the number of Monte Carlo steps required for the autocorrelator to drop to 1/e of its initial value. The initial \( \tau \) steps of a Monte Carlo run were discarded, and subsequent parameter sets separated by \( \tau \) samples were kept for analysis. The ground state Hessian matrix \( H \) has elements given by

\[ H_{ij} = \frac{\partial^2 C(p)}{\partial \log p_i \partial \log p_j} \bigg|_{p=p^*}. \]

We compute the ground state Hessian by finite differences, centered at the best fit parameters \( p^* \). We use a stepsize for finite differencing chosen to minimize the sum of truncation and roundoff errors (Press et al. 1996). We diagonalize this matrix to obtain \( V \), the matrix of eigenvectors of \( H \). The eigenparameters \( \alpha_j \), which are simply the coordinates of the ensemble bare parameter sets along the eigendirections of the ground state Hessian, are given by

\[ \alpha_j = \sum_{i=1}^{N_p} V_{ji} \log(p_i/p_i^*), \]

where \( V_{ji} \) are the elements of \( V \), \( p_i^* \) is the ground state (best fit) parameter value and \( N_p \) is the number of parameters (48 for the PC12 cell model). Explicitly, according to our formula in (5), the eigenparameters are linear combinations of the natural logarithms of shifts in rate constants, or equivalently, ratios of rate constants raised to powers, which we can show by rewriting (5) as

\[ e^\alpha_j = \prod_{i=1}^{N_p} p_i^{V_{ji}}. \]

In either eigenparameter representation (equation (5) or equation (6)), changing the combination of bare rate constants described by \( \alpha_j \) has a cost proportional to the \( j \)th eigenvalue of the Hessian matrix, at least in the harmonic approximation.

9 See the website http://www.las.dcls.cornell.edu/sethna/GeneDynamics/.
2.4. Mapping eigenvectors to data points

To determine which data points are most perturbed by motion in an eigendirection, we Taylor expand the deviation of the model from the data

\[ r_i = y(x_i, p) - Y_i \] (7)

about the minimum, which involves the Jacobian matrix of the deviations with respect to the model’s (log) parameters. The Jacobian’s elements are given by

\[ J_{ij} = \frac{\partial r_i}{\partial \log p_j} \] (8)

The product of this Jacobian and the matrix of eigenvectors

\[ d_{ik} = J_{ij} v_{kj} \] (9)

tells us exactly where the model/data agreement becomes poor as we move in any eigendirection. If \( d_{ik} \) is large, then agreement with data point \( i \) will be changed by movement in direction \( v_k \). If \( d_{ik} \) is near zero, the ability of the model to fit data point \( i \) will show no sensitivity to motions in parameter direction \( v_k \). As expected, if index \( k \) corresponds to a very soft mode, \( d_{ik} \) tends to be small for all \( i \).

2.5. Cell culture and protein detection

Rat pheochromocytoma (PC12) cells were maintained in RPMI 1640 (Gibco, Herndon, VA) supplemented with 10% horse serum, 5% calf serum (both from GibcoBRL, Gaithersburg, MD) and antibiotics/antimycotics at 1:1000. Sixteen hours prior to treatment with either EGF or NGF (both Gibco), cells were resuspended in serum-free RPMI. If LY294002 (Calbiochem, La Jolla, CA) was used, it was added to the medium 2 h prior to growth factor treatment. Cells were lysed and samples analysed by SDS-PAGE. Proteins were transferred to nitrocellulose membranes (NEN, Boston, MA) and probed with anti-active Erk1/2 and anti-Erk1/2 (both antibodies from Cell Signaling Technologies, Beverly, MA). Detection was via chemiluminescence (ECL reagent, Amersham Life Sciences, Buckinghamshire, England).

3. Results and discussion

3.1. The system and model

We have chosen nerve growth factor (NGF) versus epidermal growth factor (EGF) stimulated signaling activities in rat pheochromocytoma (PC12) cells as an initial experimental system to test our modeling approach. Pheochromocytoma cells have proven to be an invaluable model system to test our modeling approach. Pheochromocytoma cells are a well-characterized model system in neuroscience (Greene and Tischler 1976), because they express both EGF receptors (EGFR) and NGF receptors (NGFR) (specifically the high-affinity TrkA receptor) and will proliferate in response to EGF treatment and differentiate into sympathetic neurons in response to prolonged treatment with NGF. It was previously reported that the activation state of extracellular regulated kinases (Erks) 1 and 2 is correlated with the cellular growth state of PC12 cells (Traverse et al 1992). A transient activation of Erk1/2 has been associated with EGF treatment and cell proliferation, while a sustained activity has been linked to NGF stimulation and differentiation. Sustained Erk1/2 phosphorylation has been suggested to be sufficient for PC12 cell differentiation (Robinson et al 1998). It has since been recognized that while both EGF and NGF receptors activate the GTP-binding protein Ras, the distinct cellular outcomes triggered by these growth factors must lie in the differential activation of other pathways that modulate Erk1/2 activity, and several hypotheses have been proposed to account for this signaling specificity (chu Kao et al 2001, York et al 1998, Yasui et al 2001, Wixler et al 1996, Brightman and Fell 2000). Figure 1 shows the topology of a model for this process (additional details are provided in the online supplementary material). The model not only includes a common pathway to Erk through Ras shared by both the EGFR and NGFR, but also includes...
two side branches that we hypothesized were important in modulating signaling. One, through phosphatidylinositol 3-OH kinase (PI3K), can serve to downregulate Erk via the negative regulation of Raf1 (Zimmermann and Moelling 1999, Rommel et al 1999), and a second, putatively through the small GTP-binding protein Rap1 and the kinase B-Raf, can upregulate Erk by boosting Mek activation (Ohtsuka et al 1996, York et al 1998, Bos et al 2001). The model presented in figure 1 is described by a set of 28 nonlinear differential equations (of which 15 are linearly independent) and has 48 rate parameters (supplementary material)\(^\text{10}\) for which precise measurements are largely unavailable.

The growth factor-stimulated dimerization of EGFRs and NGFRs is not explicitly depicted in the model, but because it is directly linked to the triggering of the downstream signaling pathways, it is an implicit component of the receptor activation steps in our analysis. The same is true for the adaptors (e.g., Grb2 for growth factor receptor-binding protein 2) that interface the EGFRs and NGFRs with mSos (for mammalian Son-of-sevenless). While there are several points in the model where the signaling activities are subject to negative regulation, for example through the actions of GTPase-activating proteins for Ras and Rap1 and phosphatases for Raf1, B-Raf, Mek1/2 and Erk1/2, we recognize that there are other points in the network where negative regulation can also occur (e.g., at the level of Akt/PKB or p90/RSK). These are not specifically depicted in the model shown in figure 1, because we assumed that these additional negative regulatory steps would not influence our interpretation of the time series of EGF- and NGF-stimulated ERK1/2 activation. The same is true for EGFR downregulation which occurs on a slower time scale than the time course for the EGF-dependent stimulation of the Ras–Raf–Mek–Erk pathway. However, it is relatively easy to incorporate these or other steps that might be identified in the future as being potentially important. Moreover, as alluded to above, we firmly believe that the most important goals of our analyses are to establish if useful predictions for complex signaling networks can be extracted using the methodology described here, as well as determine just how well a particular network explains available experimental data, or if in fact additional interactions and signaling participants are necessary.

3.2. The ensemble approach to modeling complex signaling networks

In the analysis presented here, we primarily use the ensemble method to match the model to time courses of the activities of signaling molecules, although the method can easily incorporate agreement with parameter measurements as well. Time series have two major benefits: one, they are often more plentiful than measurements of kinetic parameters, and two, they are independent of the mathematical form of the model (for example, particular kinetic schemes). Because of the significant degree of indeterminacy in the model, a single set of parameters forms an incomplete description. Thus, a thermal Monte Carlo (Metropolis et al 1953,\(^\text{10}\) We include the saturation \(K_{\text{sat}}\) with the rate constants.\(^{10}\)\(^{10}\) We include the saturation \(K_{\text{sat}}\) with the rate constants.

![Figure 2](image_url)  
Figure 2. Behavior of the PC12 cell model. (a) Ensemble of acceptable solutions for the model with topology given in figure 1. Means and sample standard deviations are calculated as described in the text from a 704-member ensemble of independent samples. Together with the data shown (Traverse et al 1994), fourteen data sets from seven experiments performed in four laboratories were used in ensemble generation (see online supplementary material). The error bars here and in subsequent figures represent one standard deviation, or the 66% confidence level (in contrast to the four standard deviation ranges in Battogtokh et al (2002)). Notice that EGF stimulates a transient Erk response (leading to proliferation) and NGF stimulates a sustained response (leading to differentiation). (b) Scatterplot of the eigenparameters (defined in (5)) for the 704-member ensemble. We begin our Monte Carlo runs at the best fit, so these plots show the amount of drift around the best fit parameters in each eigendirection. The eigenparameters from the ensemble densely populate the area covered by the colored bars, which extend from the minimum value in the ensemble to the maximum value. The scale for the y axis is the natural logarithm (base \(e\)). Stiff eigenparameters exhibit small fluctuations (short bars) and soft eigenparameters exhibit large fluctuations (tall bars). Notice that while the eigenparameters vary over several orders of magnitude, the variation in Erk1/2 activity shown in (a) is small. The variation of the softest eigenvalues in complete equilibrium is likely even larger.

Newman and Barkema 1999, Hastings 1970, Battogtokh et al 2002, Brown and Sethna 2003) is used to generate an ensemble of parameters weighted by cost, from which we can compute a mean and standard deviation for the activity of each protein (see ‘experimental section’ as well as the discussion of figure 2(a)). Of particular importance is the standard deviation of the activity, because it is a direct measure of how perturbations of the parameters affect predictions of the model.
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\[ \log(H_{nn}/2) \]

\[ \log(H_{nn}/2) \]

\[ \log(H_{nn}/2) \]

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\[ \log(H_{nn}/2) \]

Figure 3. Plot showing the logarithm of the robustness (equation (1)) for each parameter of the PC12 model. In both (a) and (b), bars that fall below the dotted line correspond to robust parameters and bars above the dotted line are nonrobust parameters (see ‘experimental section’ for more details). Note the different scales in (a) and (b). White bars in the bar graphs correspond to diagonal elements \( H_{nn} \) that have (small) negative values; in these cases the plot displays the log of the absolute value. Color coding (see online version) of the networks indicates experimental data sets that were present for Hessian computation; proteins for which EGF-response data were used are colored in magenta and those for which NGF-response data were used are colored in green. (a) In the case where we have constraining data available for many proteins in the network, we are probing the sensitivity of a multifunctional object to parameter variations and find a very nonrobust system; 37 out of the 48 parameters lie above our line of significance. (b) When we view the network as an input/output transducer with Erk1/2 activation as the output, we find a very robust result; 39 of the 48 parameters can be varied by a factor of 2 with no significant effect on the network output. These diagonal elements are calculated using finite differences at the optimal stepsize, and are dependent on the numerical integration scheme, stepsize and quality of the minimum.

The ensemble method simultaneously makes the model more useful and falsifiable. If the variation in a particular chemical activity is large across the ensemble, then predictions based on that outcome are unreliable—the model is not sufficiently constrained to make a useful statement about such a situation. Conversely, when a single parameter set is used to characterize the model, it might accommodate new data simply by wiggling some of the parameter combinations, and thereby provide an unreliable description of the system. When using the ensemble approach, new data that fall far outside the ensemble prediction illustrate a feature of the system that the model is incapable of representing.\(^{11}\)

Figure 2(a) shows the results of the ensemble approach applied to the PC12 cell system. The figure illustrates the active Erk1/2 response to EGF and NGF. In all, fourteen chemical times series from seven experiments performed in four laboratories were used for ensemble generation (see supplemental material). As discussed above, rather than displaying a single fit, an average over many fits is presented, for which the details are as follows. To quantitatively compare the model’s output to data, a least-squares cost function is used

\[
C(p) = \frac{1}{2} \sum_{k=1}^{N_k} \sum_{i=1}^{N_i} \left( \frac{R_k y_k(t_i, p) - Y_{ik}}{\sigma_{ik}} \right)^2, \tag{10}
\]

where \( Y_{ik}, \sigma_{ik} \) are the value and error of the \( i \)th data point in the \( k \)th time series, \( y_k(t_i, p) \) is the model output for the \( k \)th time series evaluated with parameter set \( p \) at time \( t_i \). The total number of experimental data points \( N_k \) is given by \( N_k = \sum_{i=1}^{N_i} N_i \), where \( N_i \) is the total number of chemical time series and \( N_k \) is the number of data points in the \( k \)th series. In particular, a typical \( p_i \) might be a binding constant for a receptor-ligand interaction or a Michaelis constant for an enzymatic step, while a data point \( Y_{ik} \) might be the

\(^{11}\) These methods identify typical members of the ensemble, however, not all members of the ensemble. New data outside the original error bars may in principle be consistent with the model but restrict the parameters to a previously insignificant subregion.
concentration of a phosphorylated protein at \(t_i = 30\) min (see figure 2(a)) with error bar \(\sigma_{ij}\) and \(y_j(t_i, p)\) would be the theory curve for that same phosphorylated protein at the same time. We introduce the factor \(B_k\) for the \(k\)th chemical time series\(^{12}\), which is an overall scaling factor for the theory curve, in order to accommodate experimental data sets with a variety of units. It is worth emphasizing that while time series measurements are the focus of this study, virtually any type of data (for example, dose–response information or experimental measurements of parameter values) can easily be incorporated into such a framework, though the notation for equation (10) might need to be modified.

The theory curves in figure 2 are given by the continuous solid and dotted curves; in this and subsequent figures showing ensemble activation curves, the central curve is the ensemble mean and the curves surrounding it show one standard deviation. It is clear from figure 2(a) that the model reproduces the expected activation of Erk1/2 by EGF and NGF.

3.3. Implications for modeling complex signaling networks: inherent sloppiness of signal transduction

Our analysis, within the context of the PC12 cell system, yields a number of interesting implications regarding the complex networks used to propagate cellular signals. One such implication becomes evident when considering to what degree particular combinations of rate constants (rather than single rate constants) can be shifted in our model and still yield a good description for the Erk activity profiles. We refer to this property as ‘sloppiness’.

A simple example is as follows. A standard first-order protein binding reaction may be characterized by two rate constants: \(k_{aa}\) and \(k_{off}\). However, in many contexts it is not these individual rate constants that are most relevant but instead the equilibrium constant \(K_d = k_{on}/k_{off}\), a measure of the affinity of the interaction. If indeed only the ratio of the on and off rates matters, then their product will be irrelevant: both rates can be increased by the same factor (a twofold increase in both, for example) and \(K_d\) will not change. For such a case, we would call \(K_d\) ‘stiff,’ because it cannot be changed without noticeable biological effects, while the product \(k_{on}k_{off}\) will be ‘soft,’ since it can be changed freely.

Rather than arbitrary ratios and products of rate constants, we analyse the fluctuations in a particular set of rate constant combinations: the eigenvectors of the Hessian matrix of the cost, expressed in terms of the logs of the rate constants (see ‘experimental section’). These particular vectors in parameter space and the degrees to which they can change while still preserving the appropriate biological response give us information about key degrees of freedom in the model. A paramount feature of the eigenvectors is that they are a unique set of alternate model parameters that show no covariance; they are independent in a way that single rate constants and other noneigenvector combinations are not. Unlike in the simple example given above, the eigenvectors are typically combinations of more than two rates (see ‘experimental section’), but one can interpret them in a similar light: the eigenvectors are particular combinations (ratios and products) of rate constants that may be individually varied. Changes in the stiff directions cause large perturbations in the system’s behavior while changes in the soft directions are imperceptible.

We note here that analysis of a system in terms of eigenparameters is standard practice in physics, and we feel it is especially useful when analysing models of signal transduction for a number of reasons. First and perhaps most importantly, the character of the eigenparameter fluctuations (figure 2(b)) is what allows us to make predictions. While individual rate parameters flop around hopelessly, we see in the stiff eigenparameters that some degrees of freedom are reasonably well constrained by the data. Our ability to determine these few stiff eigenvectors well is what allows us to make any predictions at all, even in the face of many unknowns (also, see the ‘robustness’ section and figure 4 for more discussion on this point). Second, and as will be considered further below (see the next section) the eigenparameters can have a physical interpretation that can decompose the system into dynamical modules (this kind of interpretation is similar to the meaning given to the dissociation constant above).

Third, analysis of the eigenparameters and their corresponding eigenvalues allows us to see similarities among seemingly unrelated models (Brown and Sethna, in preparation).

An eigenvector analysis is shown in figure 2(b) which plots linear combinations of the natural logarithms of shifts in rate constants (see ‘experimental section’ for a full description). The relatively large size of the vertical bars for the majority of the eigenparameters in figure 2(b) (note the natural log scale of the vertical axis) indicates that only a small fraction of parameter combinations are well constrained by the data (these are the aforementioned ‘stiff modes’—also, see the next section). The majority of the eigenparameters (around 80%) are ‘soft’ and vary over more than an order of magnitude and sometimes many orders of magnitude. We emphasize that this softness is not tied to an obvious underdetermination of parameters, as (i) 59 parameters (rate constants plus \(B_k\) in (10) were fit to 68 data points in figure 2 and (ii) while there are many protein activities for which we have no direct data, the eigenvalue spectrum still spans orders of magnitude even when we construct an artificial situation by generating, from the model itself, an abundance of ‘perfect data’ for every chemical species (Brown and Sethna 2003). The ‘perfect data’ exercise also reveals the quantity and quality (both high) of data necessary to accurately determine even a fraction of the individual rate constants, which is why we confine our predictions to chemical activities and not rate constant values.

Figure 2(b) provides a strong argument for the ensemble approach, as the huge variation in eigenparameters makes description of a complex cellular signaling network with a single set of ‘best’ parameters perilous.

3.4. Implications for modeling complex signaling networks: only a few parameter combinations are ‘stiff’

Another important implication for complex cellular signaling networks that emerges from our analysis is that only a

\(^{12}\) While the word ‘chemicals’ could denote proteins, RNA, small molecules, etc, for purposes of this study all the chemicals are proteins, sometimes separated into different phosphorylation or GTP-binding states.
Figure 4. Schematic illustrating the difference between robustness range, parameter error bars and stiff and soft eigendirections, all of which are forms of parameter variation discussed in the text. The black ellipses represent lines of equal cost for a simple quadratic cost function with only two parameters, $k_1$ and $k_2$. The best fit (minimum cost) is positioned where the green and blue axes cross. The blue axes (whose tips are labeled $r_1$ and $r_2$) show the robustness range of the two parameters, for a quantitative robustness definition similar to the one described in the text. The red dotted lines and arrows (labeled $s_1$ and $s_2$) give the error bars for the parameters. Notice that the parameter error bars are larger than the robustness range: unless the rate constants show no covariance (the axes of the ellipse coincide with the black axes labeled $\log k_1$ and $\log k_2$) this will be the case. The green axes show the range of the two eigenparameters; notice that one eigenparameter ($v_1$) has a much smaller range of variation than the error bar or robustness range of either parameter, and one eigenparameter ($v_2$) has a much larger range of variation. We would call $v_1$ stiff and $v_2$ soft. This schematic differs from the actual behavior of our model near the cost minimum in three significant ways. First, the schematic shows only two dimensions, rather than 48 for the PC12 model. Second, the model shows perfect ellipses, ignoring the nonlinearities that make stochastic sampling a necessity. Third, typical elliptical contours in the PC12 model are vastly more eccentric (needle-like): the robustness range (blue) is typically less than a factor of 2, while the error bars (red) are all larger than a factor of 1000.

small fraction of parameter combinations are important in determining the behavior of the signaling system that we are studying. It is this property—that only a few eigendirections capture most of the dynamical behavior—that we take as the definition of ‘sloppy.’ One may go one step further and naturally ask: what are these combinations? Which rate constants appear in the ‘stiff degrees of freedom’? The stiffest mode corresponds approximately to the parameter combination ($k_{\text{GAP}} k_{\text{Ras}}/k_{\text{Sos}} k_{\text{Raf}} K_{mSos}$), which is a ratio of rate constants that antagonize Ras and Raf functions (e.g., the rate for GAP-catalyzed deactivation of Ras and the deactivation rate for Raf) to those that promote it (activation of Ras by Sos, activation of Raf by Ras and the $K_{m}$ for RasGAP-catalyzed GTP hydrolysis). This points to Ras and Raf as the critical nexus for generating the appropriate signaling behavior. Perhaps not surprisingly, the proteins which emerge as the key control points in our model are indeed those, when mutated, that are most likely to cause disease. We emphasize that we have arrived at this conclusion—that Ras and Raf are key in the network—solely through the coupling of the model to time series data for a variety of proteins, not just Ras and Raf. This points to the power of stiff mode analysis in highlighting key proteins and interactions, which would be particularly valuable in cases where such key regulators are not yet known experimentally. The second stiffest mode predominantly involves rates that localize to the feedback loop from Erk to p90/RSK to mSos (figure 1); it is the ratio of the $K_{m}$ for p90/RSK activation and Sos deactivation to the same activation/deactivation rates ($k_{s8}$). This highlights negative feedback from Erk to Sos as a second key point for regulation in the network.

We can go beyond simply identifying those parameter combinations that need to be tightly constrained to asking the question: if we move in a stiff direction, where does the model begin to miss the data most significantly? We investigate this by Taylor expansion of the deviation of the model from the data (see ‘experimental section’). We find that the stiffest mode—the one localizing to Ras and Raf—is most important in achieving the correct fast response, on the scale of a few minutes, for many proteins under the regulation of both growth factors. The second stiffest mode when perturbed, on the other hand, has a dramatic effect on Ras activity on longer timescales (30 min) and also regulates Rap1 activity (i.e. the second stiffest mode mixes rates from the Rap1 loop with those in the feedback loop from Erk to mSos). Thus, the identity of the stiff eigenvectors points to key control points in the signaling network. Moreover, because the dominant rate constants in the stiffest eigenvectors do not have to appear close to each other in the network, the stiffest eigenvectors can identify ‘dynamical modules’ that mix multiple static protein modules. Finally and perhaps most importantly, mapping eigenvector perturbations back to the data shows what aspects of the temporal profile are affected by disruption of these critical regulatory groups and can suggest manipulations that would ‘tune’ the system to a particular response.

3.5. Implications for modeling complex signaling networks: robustness

Using the ensemble approach to analyse the PC12 cell signaling model also allows us to ask questions about the sensitivity of the network’s activity to changes in single (rate) parameters. Since its introduction (Barkai and Leibler 1997), the term ‘robustness’ has acquired a number of definitions; here we follow others (von Dassow et al 2000, Smith et al 2002, Laub and Loomis 1998) in defining robustness as the sensitivity of a network’s behavior to changes in single parameters. We note the difference between this property and sloppiness—sloppiness is concerned with fluctuations along eigendirections, which are particular parameter combinations. Figure 3(a) shows our results for the robustness of the PC12 cell network, with details for the calculation presented in the
figure legend and in ‘experimental section.’ The dotted line in
the figure sets the value of a calibration scale; every bar falling
below the dotted line corresponds to a robust parameter, and
those falling above are nonrobust. In addition, the relative
robustness or nonrobustness of a parameter is given by the
height of its corresponding vertical bar—a bar that is half
as high as another indicates the former parameter is twice
as robust as the latter. We can see that when we take into
account the activities of all the proteins included in our full
experimental data set, the model is quite nonrobust, since
changes in 80% of the parameters result in significantly worse
agreement with data (figure 3(a)).

The fact that our model is not very robust is both
because we have a quantitative measure of model agreement
(equation (10)) rather than ‘fit by eye’) and because we
consider more than a single output or behavior of the model,
since we have data for the active forms of six of the proteins
of the PC12 cell model, some for both EGF and NGF treatments.
Thus, we have a rather stringent criterion for model success.
However, this picture changes dramatically if we consider
the system in terms of a simple ‘input/output’ relationship. For
example, if we consider only Erk activation by EGF and NGF
as the pertinent outputs, we see a much more robust response,
finding in this case only 9 nonrobust parameters rather than 37
(see figure 3(b)). While in some cases viewing biochemical
systems as input/output transducers is justified, in others it is
not a realistic description. For example, the Ras protein has a
myriad of cellular targets (Vojtek and Der 1998) and in many
cases, the physiological roles of Ras in the cell may require
its stimulation of multiple targets/effectors as well as complex
‘cross-talk’ between these different effectors.

Overall, we feel that our simple definition of robustness
offered in (1) (‘experimental section’) and the subsequent
discussion gives a quantitative measure of what one means
by robustness at any level of detail, whether one is interested
in input/output characteristics (figure 3(b)), the behavior of
several internal network components (figure 3(a)), or a level
of description somewhere in between (two outputs rather than
one, for example). However, it is important to appreciate
the differences between the robustness of a parameter, a
parameter’s error bar (as obtained from the formal covariance
matrix of the fit (Press et al 1996)), and the ranges of the
eigenparameters (as shown in figure 2(b)). When we examine
the error bars on the fitted parameters for the PC12 cell model,
we find them to be huge: the most well-defined rate constant
has an error bar of 10³. The schematic in figure 4 provides
an example of the differences that can occur with regard to
the relative robustness versus the size of the error bars for a
simple two-parameter case, where in this example the range
for the error bars (schematically indicated by the red dotted
lines and arrows labeled ‘s1’ and ‘s2’) is much larger than the
typical ‘robustness range’ (illustrated by the blue axes with tips
labeled ‘r1’ and ‘r2’). This example, described in more detail
in the legend to figure 4, immediately begs two questions:
(1) How do we understand the enormous error bars on the
rate constants? (2) How can we hope to generate any useful
predictions from models of cellular signaling systems, given
the large ranges on parameter values that can and do occur?

Figure 4 helps to provide answers to both of these
questions. First, we see that there is no contradiction in having
a parameter’s error bar be much larger than its robustness
range; as the ellipses in figure 4 become more stretched, the
error bars on the parameters grow while their robustness ranges
remain roughly the same. Secondly, and more importantly,
the eigenvectors illustrate how it is that we can make any
predictions at all. While the individual rate constants may
all have huge error bars, the same need not be true of the
eigenvectors. Some eigenvectors (v2 in figure 4) can be even
more poorly determined than the worst-constrained single
parameter, but some (like v1) can be much better determined
than even the most well-constrained parameter in the model.

Thus, in summary the parameter ranges obtained from
our robustness calculation assume that a parameter value
is changed singly while others remain fixed. In a formal
covariance calculation, the fact that other parameters may shift
to compensate for part of the change in a single parameter
leads to larger error ranges: for example, there may be
more variation because other parameters are able to offset
a change in a given rate constant. The eigenvector ranges also
assume more than one rate constant can be moved at once,
but eigenvectors are very particular combinations: motions
in one eigendirection cannot be offset or compensated by
motions in any other eigendirection. In practical terms, the
questions of most pressing biological interest are not rate
constant values but changes in cellular behavior upon different
interventions and mutations. We will see in the next section
that these biologically relevant quantities are well predicted
by our model, despite the fact that we have shown that we cannot
predict reaction rate constants with our time series data.

3.6. Predictions and experimental verification

An important goal is to use our model to make testable
predictions about biological or cellular experiments for which
we have no results. For the PC12 cell signaling network, we
have hypothesized that the left arm of the pathway (see figure 1)
is suppressing Erk1/2 activation by EGF. However, what do
we predict when PI3K is not activated? If PI3K activation
is critical to the transient activation of Erk1/2 by EGF,
then inhibition of PI3K might cause sustained Erk1/2
activation and give rise to cellular differentiation. If this
were true, then it should be possible to convert EGF to a
differentiating factor using the PI3K pathway. Figure 5(a)
shows an ensemble prediction for the time series of Erk1/2
in response to EGF, under conditions where PI3K activity
has been inhibited. We were quite surprised to find that the model
predicts the opposite of our initial expectation, namely that
PI3K inhibition will not lead to differentiation in response
to EGF. We emphasize that this is not a prediction of only a
single set of parameters: this approach examines a sampling of
all parameters consistent with available time-series data. It is
particularly noteworthy that precise predictions of biologically
relevant time series data can be reliably extracted from a model
whose rate constants are each varying over many orders of
magnitude.

Figure 6 shows the results obtained from experiments
using LY294002, a pharmacological inhibitor of PI3K. The
qualitative agreement between model and experiment is quite good, and both clearly show that the inhibition of PI3K activity neither produces a sustained Erk1/2 signal in response to EGF nor does it switch the NGF-induced Erk1/2 activation profile from a sustained to a transient response (although it does provide some quantitative tuning of the signal at short times). Also, the inhibition of PI3K activity does not cause significant morphological differentiation in combination with EGF treatment (supplemental material), as expected from the relationship between sustained Erk1/2 activity and differentiation.

In particular, these analyses suggest that the PI3K to Akt loop in figure 1 (shown as grayed-out) is not necessary to account for the differences in Erk1/2 activation in response to EGF versus NGF. This is further supported by the cluster of ‘irrelevant’ rate constants near rate constant number 30 in figures 3(a) and (b), since they are all associated with this loop. Indeed, such a reduced model, generated by removing the PI3K to Akt loop, describes the Erk1/2 data (and the rest of the data used in this study) only slightly worse than the larger model, yielding an optimal cost that is about 30% higher, and similar ensemble predictions.

We also make predictions about manipulations that, unlike inhibition of PI3K, do dramatically affect Erk activation. Figure 5(b) shows the Erk response in PC12 cells to 50 ng ml⁻¹ NGF and either dominant negative (DN) Ras (blue curve) or Rap1 (red curve), a member of the Ras family of GTP-binding proteins that like Ras is activated by the NGF receptor. These predictions show good qualitative agreement with previous experiments (York et al 1998), in which DNRas interferes with early Erk activation but not its eventual sustained behavior and DN Rap1 affects the long-term value of Erk phosphorylation but not its early activation. Thus, taken together, figures 5 and 6 show that our model agrees with, and can predict the results of, experimental manipulations that disrupt each of the three main pathways we have included in our model: PI3K, Rap1 and Ras.

4. Conclusion and outlook

In conclusion, motivated by ideas from physics, we have used a formalism (part of which is termed elsewhere the ensemble
method (Battogtokh et al 2002)) for modeling cellular signaling networks that (1) provides biologically accurate descriptions of the signal output, and (2) is falsifiable even in the face of a high degree of uncertainty regarding the rates and binding affinities for many of the steps comprising complex biological systems. We have applied this methodology to the signaling systems that underlie NGF-induced neurite extension and differentiation of PC12 cells and have been able to evaluate the importance of different regulatory loops in generating the key signaling endpoint, the sustained activation of Erk. However, what may be most important, our modeling efforts have yielded some interesting and perhaps previously unappreciated implications and lead us to emphasize some key points regarding complex cellular signaling networks. First, it is clear that only a small fraction of parameter combinations (the eigenparameters) for such signaling systems are likely to be well constrained, and most if not all individual rate constants can vary over huge ranges. In fact, some of the error bars for the individual rate constants can be enormous even though the sensitivity of the system to a change in these parameters is high (i.e. even when the parameters are not robust) due to covariance of other rate constants that can compensate. Second, the few well-constrained (stiff) parameters reveal critical focal points in the signaling network for ensuring the generation of an appropriate output; in the case of the PC12 cell system, the stiffest mode encompasses the regulation of Ras and Raf, two proteins which are well known for playing crucial regulatory roles in mitogenic pathways, as well as in cellular differentiation, and when mutated, stimulate oncogenic transformation.

Overall, this now leads to our appreciation that complex signaling systems are characterized by an inherent sloppiness such that a limited number of parameter combinations (the stiff eigenvectors) are sufficient to generate the observed signaling behavior. As a corollary, there are many parameter combinations that can undergo marked variation yet yield similar signaling outputs and end results. This offers some intriguing possibilities regarding the way in which signaling systems with multiple interacting pathways can evolve. Indeed, we believe our analysis yields insights into one way in which properties like robustness and evolvability can simultaneously coexist. Soft modes show a property similar to that of robust rate parameters, as soft modes can absorb large changes without altering cellular behavior. In contrast, even small motions in the stiff modes can elicit large effects in cellular signaling. Hence, when considering the effects of multiple genetic mutations, perturbations in some combinations (the stiff modes) allow the organism to adapt to new conditions while fluctuation in others (the soft modes) leaves critical signaling activities intact and unperturbed.

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**Glossary**

**Cellular signaling.** Chemical computations performed by diverse proteins in the cell through a sequence of post-translational modifications (i.e. phosphorylation), protein–protein interactions and small molecule binding (i.e. GTP binding) that couple changes in the transcriptional program of a cell to environmental stimuli.

**EGF.** Epidermal growth factor. A ligand that, when binding to its receptor on the cell surface, initiates a cascade of molecular events resulting in cell proliferation.

**Eigenvectors/eigenvalues.** If for a matrix \( A \) and vector \( v \) one has \( Av = \lambda v \), then \( v \) is an eigenvector of \( A \) with \( \lambda \) its eigenvalue. Square \( N \times N \) matrices will have \( N \) such eigenvalues (not necessarily all real or distinct) and \( N \) corresponding eigenvectors.

**Erk1/2.** Extracellular regulated Kinases 1 and 2. A mitogen activated protein kinase (MAP Kinase) phosphorylated in response to diverse growth factors and cellular stimuli.

**Falsifying a model.** Given a network topology and mathematical model for its interactions, we say a model is invalid if the parameter ensemble shows significant deviations either from existing experimental data or new experiments suggested by model predictions. This form of model failure suggests that changing parameters is insufficient to fix the model-data discrepancy, but it makes no statement about the effects of changes in model topology or form, which could correct the discrepancy.

**NGF.** Nerve growth factor: a ligand that, when binding to its receptor on the cell surface, initiates a cascade of molecular events leading to growth arrest and subsequent differentiation into a neuronal phenotype.

**PC12 cells.** Rat pheochromocytoma cells. A cell culture line that responds to both EGF and NGF (as well as other growth factors), and has often been utilized as a model system to study neuronal differentiation.

**Robustness.** The lack of sensitivity of a signaling network’s behavior to changes in individual reaction rate (or other such) parameters.

**Saturable reaction forms.** The classical Michaelis–Menten enzymatic reaction is an example of such a chemical reaction: the reaction rate initially increases with the addition of more substrate, but eventually reaches a finite value (saturates) in which more substrate does not result in a further increase in reaction rate.

**Sloppiness.** A term introduced by us in this paper. The property that only a few (of very many) eigendirections...
capture almost all of the dynamical behavior of a signaling network.

**Stiff/soft directions/eigenvectors.** Vector directions in multidimensional parameter space; in the case of stiff directions, small perturbations in those directions cause dramatic perturbations to the network’s behavior. In the case of soft directions, large perturbations can be tolerated with little or no change in the network dynamical behavior.

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