A simple model for $1/f^\alpha$ noise

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We present a simple stochastic mechanism which generates pulse trains exhibiting a power law distribution of the pulse intervals and a $1/f^\alpha$ power spectrum over several decades at low frequencies with $\alpha$ close to one. The essential ingredient of our model is a fluctuating threshold which performs a Brownian motion. Whenever an increasing potential $V(t)$ hits the threshold, $V(t)$ is reset to the origin and a pulse is emitted. We show that if $V(t)$ increases linearly in time, the pulse intervals can be approximated by a random walk with multiplicative noise. Our model agrees with recent experiments in neurobiology and explains the high interpulse interval variability and the occurrence of $1/f^\alpha$ noise observed in cortical neurons and earthquake data.

The omnipresence of $1/f^\alpha$ noise in nature is one of the oldest puzzles in contemporary physics still lacking a generally accepted explanation. The phenomenon is characterized by a certain behavior of the respective time signal: The power spectrum $S(f)$ is proportional to $1/f^\alpha$ at low frequencies $f$ with $\alpha \approx 1$. Examples include the light of quasars [1], electrical measurements [2], music and speech [3], human cognition [4] and coordination [5], the current through ion channels [6], network traffic [7], burst errors in communication systems [8], freeway traffic [9], granular flow [10], etc. The time signals of a large number of these systems [11–15] resemble a pulse train consisting of individual, largely identical events which occur at discrete times. This is especially true for spike trains of single nerve cells for which $1/f^\alpha$ noise has been observed in various brain structures [11–15]. The reported exponents, which depend both on the presence or absence of a sensory stimulus [11,12] and on the state of the animal (REM sleep vs awake state) [13,14], vary from 0.68 to 1.38. The power-law behavior for spike train power spectra lies within the range 0.01 to 10 Hz, extending typically over 2 decades. In almost all cases the upper limit of the observed time over which fractal correlations exist is imposed by the duration of the recording.

In this Letter, we propose a simple mechanism for generating pulse trains with $1/f^\alpha$ behavior in systems with a threshold-controlled dynamics like, e.g., neurons and earthquake faults. Our model is based on an integrate-and-fire (IAF) mechanism and consists of a single unit characterized by two variables (see Fig. 1): The voltage $V(t)$ and the threshold $C(t)$. Initially, the voltage is below the threshold. Then, the voltage increases monotonically in time — in the simplest case just linearly — and the threshold evolves according to a Brownian motion with diffusion constant $D$ within reflecting boundaries $V_0 < C_1 < C(t) < C_u$. As soon as $V(t)$ has reached the threshold, the voltage is reset to $V_0$ and a pulse of unit height is emitted. In this way, a pulse train is generated. Note that the threshold is not reset to its initial value.

Such a model is often used to describe single neurons: $V(t)$ is the membrane potential and the emitted pulse is the generated action potential. However, it is usually assumed that the threshold is constant in time. Recent investigation have shown that this is not true for cortical neurons in vivo [16] and in vitro [17]. Additionally, there is evidence that the spike trains of auditory neurons [18] and of neurons in the mesencephalic reticular formation [19] are not renewal, i.e., successive time intervals between spikes are correlated. These facts are incorporated in our model in the simplest possible way. Moreover, the effects of dead time or absolute refractoriness, which limits the rate at which a neuron can fire, are automatically included in our model via the lower bound $C_l$. The upper bound $C_u$ prevents an infinite time difference between two pulses.

![Figure 1](image-url)

FIG. 1. Dynamics of our model for a linear increasing voltage $V(t)$ with $V_0 = 0$. The dashed lines represent the lower and the upper boundary for the fluctuating threshold $C(t)$.

As one can see from Fig. 2, the power spectrum of the pulse train generated by our model with linear increasing voltage shows a $1/f^\alpha$ decay over several decades [20]. The frequency below which white noise behavior...
is observed is determined by $C_u - C_l$ and goes to zero for $C_u - C_l \to \infty$. The exponent $\alpha$ is not universal and increases if the ratio $(C_l - V_0)/\sqrt{\langle D \rangle}$ increases. In the limit $(C_l - V_0) \ll \sqrt{\langle D \rangle}$, we find $\alpha = 0.5$. This result is explained by the fact that this limit corresponds to the case in which the waiting times between pulses are purely determined by the diffusive dynamics of the threshold. Hence, each waiting time is merely the first return time of a Brownian motion which obeys a power-law distribution with exponent $-1.5$. This implies $\alpha = 0.5$.

To compare our results with real neurons, consider the parameters of curve (b): The dead time of a neuron is typically of order of milliseconds and the maximal time difference between two spikes of the order of seconds. This is exactly the ratio between $C_l$ and $C_u$. Moreover, we can now identify one unit of time in our model with 5 milliseconds real time. Hence, the $1/f^\alpha$ behavior in (b) is found for $f < 11$ Hz. This and the fact that $\alpha \approx 1.02$ reproduces the experimental results very well.

Extensive numerical investigations have shown that our model is very stable with respect to variations of the dynamics. Different forms of voltage increase, e.g., a linear, a squared, or a square-root increase, give similar results. The assumption of a monotonically increasing of the voltage can also be dropped. A small amount of noise can be added to the voltage signal without altering our findings. Substituting the reflecting boundaries by a confining potential does not change our results, either. This points towards a generic behavior.

To obtain the power spectrum of our model analytically, consider the signal $X(t) = \sum_k \delta(t - t_k)$ where $t_k$ denotes the time of occurrence of the $k$th pulse. It follows as shown in [2]

$$S(f) = \lim_{T \to \infty} \frac{1}{2T} \left| \int_{-T}^{T} dt X(t) \exp(-2\pi f t) \right|^2,$$

$$= \lim_{T \to \infty} \frac{1}{2T} \sum_k \sum_q \exp(2\pi f(t_{k+q} - t_k)). \tag{2}$$

With $I = \lim_{T \to \infty} \frac{1}{2T}(k_{\text{max}} - k_{\text{min}} + 1)$, this leads to

$$S(f) \approx I \sum_q \left\langle \exp(2\pi f(t_{k+q} - t_k)) \right\rangle, \tag{3}$$

where $\langle \cdots \rangle$ denotes the average over the ensemble and over $k$. Hence, we need to know the probability distributions $\Psi_q(\tau) d\tau$ of the time differences between pulses $\tau = t_k - t_{k+q}$ for all integers $q$. $\Psi_q$ is merely the $q$th passage times density function $g_q$ averaged over the stationary probability distribution of “initial” states $V(0)$

$$\Psi_q(\tau) = \langle g_q(\tau|V(0))\rangle_{V(0)}. \tag{4}$$

Since $g_q$ can be computed from the first passage times density function (FPTDF), we will first focus on the latter.

![FIG. 2. Power spectrum of the pulse train generated by our model. Parameters are (a): $V_0 = 0$, $C_l = 0.2$, $C_u = 40$, $\sqrt{\langle D \rangle} = 0.2$. (b) as (a) with $C_u = 200$. (c): $V_0 = 0$, $C_l = 0.02$, $C_u = 4000$, $\sqrt{\langle D \rangle} = 2.0$. This curve is shifted down by 1 decade. All curves show a clear $1/f^\alpha$ decay. $\alpha$ varies from 0.6 to 1.1.](image)

The FPTDF of our model with linear voltage increase can be obtained by mapping the model to an IAIF model with constant threshold $C = (C_u + C_l)/2$: The voltage $\tilde{V}(t)$ is defined as the sum of $V(t)$ and $C = C(t)$. This means that $\tilde{V}(t)$ fluctuates around $V(t)$. It also implies that $\tilde{V}(t)$ is reset to $V_0 + C - C(t_k)$ after the $k$th threshold crossing. Hence, the correlations are now encoded in the fluctuating reset. In conclusion, $\tilde{V}(t)$ behaves almost as a Brownian motion with drift to an absorbing barrier with a reset following each barrier crossing. The only difference is that the stochastic process is restricted to the interval $[V(t) + C - C_u, V(t) + C - C_l]$ at time $t$ which makes an exact mathematical treatment difficult. Neglecting the restriction for a moment and setting $C = 0$, we obtain from the associated Fokker-Planck equation the FPTDF

$$g_1(\tau|V(0)) = \frac{-\tilde{V}(0)}{\sqrt{2\pi D\tau^{3/2}}} \exp\left(-\frac{(\tilde{V}(0) + \tau)^2}{2D\tau}\right), \tag{5}$$

and $g_1 \equiv 0$ for $\tau < 0$. Here, $\tilde{V}(0)$ is the initial distance. Eq. (5) is, of course, just an approximation to the FPTDF of our model. This can already be seen from the fact that the FPTDF of our model is identically zero for $\tau < (C_l - V_0)$ and $\tau > (C_u - V_0)$. However, as will be shown below this approximation proves to be very useful and Eq. (5) can even be simplified to a Gaussian with the same mean and variance:

$$g_1(\tau|\tilde{V}(0)) \propto \exp\left(-\frac{(\tilde{V}(0) + \tau)^2}{2D\tilde{V}(0)}\right). \tag{6}$$

From the FPTDF one could now compute higher passage times density functions $g_n$ in principle by convolution

$$g_n(\tau|\tilde{V}(0)) = \int_0^\tau g_1(t|\tilde{V}(0))g_{n-1}(\tau - t)dt. \tag{7}$$
However, this convolution resists an analytical treatment due to the
Markovian character of our process and the form of Eqs. (8). The
former manifests itself in the fact that the first passage time directly
suggests itself as the initial distance between the threshold and the
voltage for the next passage problem. The reason for this is that the
distance of the kth reset of the voltage V equals the time
difference between the kth and the (k−1)th pulse due to
the linear increase of the voltage V with slope 1. Hence
the reset depends on the last passage time only and the
whole stochastic point process is totally described by the
FPTDF plus its Markovian property.

![FIG. 3. Power spectrum of the time signal generated by the
linear version of our model and by the two approximations for
the same parameters as in Fig. 2 (b).](image)

These properties enable us to interpret the stochastic
process generated by the Gaussian approximation (3) as
a random walk of the inter-spike-intervals (ISI) τk:

\[ \tau_{k+1} = \tau_k + \sqrt{D_\tau} \eta_k. \]

Here, \( \eta_k \) denotes the white noise source. Note the
special kind of multiplicative noise which distinguishes our
model from the one in \( \text{[25]} \). The variance of the step
length is proportional to the current “position”. Hence,
the origin is a fixed point of the random walk. To omit
this difficulty and in spirit of our original model, we con-
sider the random walk \( \tau_k \) to be confined by two reflecting
boundaries, i.e., \( 0 < (C_u - V_0) < \tau_k < (C_l - V_0) \). The
power spectrum of the pulse-train generated by such a
random walk with \( \tau_{k+1} = \tau_k + \tau_k \) shows a clear \( 1/f^\alpha \)
behavior with the same exponent as for our model (see
Fig. 3). This is also true if the new inter-spike-interval
is chosen from an inverse Gaussian distribution given in
Eq. (3) with an initial condition depending on the last
interval. Hence, these approximations seem to be justic-
tied. This is further confirmed by the stationary ISI
distribution. For the random walk, the ISI distribution
function \( P(\tau) \) is proportional to \( \tau^{-1} \). Simulations
show that this is in excellent agreement with our model
and the inverse Gaussian approximation.

We have to point out that the behavior of \( P(\tau) \) depends
on the specific kind of voltage increase. For a voltage
increase with \( (t - t_{last})^\beta \) with \( 0 < \beta < 2 \), we find
\( P(\tau) \propto \tau^{\beta-2} \) for our model. Substituting the reflect-
ing boundaries by a potential of the form \( a/x + bx^2 \) for
example, we still find power law tails in the ISI distrib-
ution. This is exactly what measurements show for cortical
neurons \( \text{[27]} \), especially in the mesencephalic reticular
formation \( \text{[14]} \). Hence, our model seems to be especially
well-suited to explain the occurrence of \( 1/f^\alpha \) noise in
that formation. In general, IaF models can not explain
the high interspike interval variability exhibited by cortical
neurons \( \text{[26]} \). A fluctuating threshold as described by
our model, however, can solve this long-standing issue.

For renewal processes the ISI distribution function and
the FPTDF are identical and completely describe the
process. This is the case for a standard IaF neuron with
reset of the voltage to the origin after each barrier cross-
ing which is described by the FPTDF in Eq. (3). Such a
model can neither explain a \( 1/f^\alpha \) signal nor a power-law
decay of the ISI distribution. In contrast to our model,
Usher and co-workers showed that fractal behavior might
be a consequence of the global activity dynamics of a
network of IaF neurons \( \text{[17]} \). Due to experimental limits-
ations, however, the link between \( 1/f^\alpha \) single-unit power
spectra and macroscopic activity dynamics remains, as of
now, a conjecture. Another attempt to explain the phe-
nomenon of \( 1/f^\alpha \) noise is based on fractal and fractal-rate
stochastic point processes \( \text{[28]} \). Certain types of these
processes properly characterize the statistical properties
found in different experiments. However, in many cases it
is not clear \textit{a priori} why the real system should generate
such a process. This is especially true for the clustering
Poisson process which was applied to explain \( 1/f^\alpha \) noise
in the mesencephalic reticular formation \( \text{[14]} \). In con-
trast to that, our model provides a simple explanation of
\( 1/f^\alpha \) noise in integrate-and-fire systems in general and,
hence, applies to neurons in particular. The crucial as-
sumption is a fluctuating threshold. Such a behavior is
related to models presented in \( \text{[29]} \) and was already con-
sidered in \( \text{[22,23]} \) to explain the power law decay of neuronal
ISI distribution functions. However, the stochastic point
process was still assumed to be renewal and could not
explain a \( 1/f^\alpha \) behavior of the power spectral density
function. Consequently, the second crucial assumption
of our model is the Markovian character of the process
in agreement with Refs. \( \text{[22,23,24]} \). To directly verify our
model for neurons in the mesencephalic reticular forma-
tion, one should measure the evolution of the reset from
the threshold potential.

All three main characteristics of our model, i.e., a \( 1/f^\alpha \)
spectrum, a power-law decay of the ISI distribution, and
a Markovian dependence of the ISI, can not only be ob-
served in nerve cells but also in other systems. For ex-
ample, the pulse signal, defined by associating the oc-
currence of pulses of unit height with earthquakes in the
and has an ISI distribution with exponent $-1.1$ (Fig. 3). Moreover, there is evidence that the ISI do not obey a renewal process. Rather a Markovian dynamics can be found. These findings imply that the effective evolution of the ISI is similar to the one generated by our model and caricatured by Eq. (8).

To summarize, we have presented a simple stochastic model which is able to transform integrated white noise with a $1/f^2$ power spectrum into noise with $1/f$ tail. The basic mechanism is similar to what is expected to describe the dynamics of single neurons and, thus, our model can explain the behavior of neurons in the central-nervous-system. The analysis of earthquake data even suggests that the effective dynamics of the ISI is the same for many systems exhibiting $1/f^\alpha$ noise.

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