Analysis of Deep Brain Stimulation Lead Targeting in the Stimulation of Anterior Nucleus of the Thalamus for Epilepsy Clinical Trial

BACKGROUND: Deep brain stimulation (DBS) of the anterior nucleus of the thalamus (ANT) is an effective therapy for patients with drug-resistant focal epilepsy. Best practices for surgical targeting of the ANT can be refined as new information becomes available regarding effective stimulation sites.

OBJECTIVE: To conduct a retrospective analysis of the relationship between outcomes (seizure reduction during year 1) and DBS lead locations in subjects from the SANTÉ pivotal trial (Stimulation of ANT for Epilepsy) based upon recent clinical findings.

METHODS: Postoperative images from SANTÉ subjects (n = 101) were evaluated with respect to lead trajectory relative to defined anatomic landmarks. A qualitative scoring system was used to rate each lead placement for proximity to an identified target region above the junction of the mammillothalamic tract with the ANT. Each subject was assigned a bilateral lead placement score, and these scores were then compared to clinical outcomes.

RESULTS: Approximately 70% of subjects had “good” bilateral lead placements based upon location with respect to the defined target. These subjects had a much higher probability of being a clinical responder (>50% seizure reduction) than those with scores reflecting suboptimal lead placements (43.5% vs 21.9%, P < .05).

CONCLUSION: Consistent with experience from more established DBS indications, our findings and other recent reports suggest that there may be specific sites within the ANT that are associated with superior clinical outcomes. It will be important to continue to evaluate these relationships and the evolution of other clinical practices (eg, programming) to further optimize this therapy.

KEY WORDS: Anterior nucleus of the thalamus, Deep brain stimulation, Epilepsy, Targeting

Deep brain stimulation (DBS) of the anterior nucleus of the thalamus (ANT) was recently approved in the United States for partial onset epilepsy. The clinical trial (Stimulation of ANT for Epilepsy, SANTÉ) supporting this therapy was initiated in 2003 with results first published in 2010. As part of the original analyses of the trial data, a detailed mapping of the active DBS contact locations was completed for each subject, using the standard anterior commissure-posterior commissure (AC-PC) based reference space, but comparison of active contact positions and clinical outcomes revealed no apparent relationship. Recently, several reports of ANT-DBS case series using advanced imaging have described considerable interpatient variability in the location of this nucleus in relationship to AC-PC reference space. In addition to the interpatient variability in position of the ANT, they also noted considerable deviation compared to the Schaltenbrand-Wahren atlas, with the nucleus located more superior and anterior in most subjects as compared to the atlas specimens.
This was notable given that, in the SANTÉ trial, indirect targeting based upon coordinates derived from the Schaltenbrand-Wahren atlas was used to guide the initial coordinates for lead placement. Finally, these groups also identified a subregion target within the ANT, superior to the mammillothalamic tract (MTT) termination, that appeared to be associated with improved outcomes. These findings prompted us to perform a post hoc re-evaluation of the lead placements to determine whether there might be a relationship between patient-specific lead locations and clinical outcomes in the SANTÉ cohort.

METHODS

The SANTÉ trial (clinicaltrials.gov, identifier NCT00101933) was approved by the institutional review board (IRB) at all study centers, and subjects provided written informed consent before participation. Per the SANTÉ protocol, all subjects (n = 110) had postoperative imaging and confirmation of bilateral DBS lead placement in the ANT before entering the randomized treatment phase. For the original assessment of lead positions, these image sets were used to determine the individual contact locations of the DBS leads (Model 3387, Medtronic) relative to the mid-commissural point (MCP) using a neuronavigation system (StealthStation™, Medronic). Active contact positions were defined in X, Y, Z space for each hemisphere, and these results were then compared to the clinical outcomes of the individual subjects, who were categorized as responders (≥50% seizure reduction) or nonresponders (<50% seizure reduction) at 1-yr postimplant. For individuals who had more than one cathode programmed on a lead (n = 81 left, n = 79 right), the active contact location was defined as the interpolation of the 2 active contact positions.

For the new analysis, lead trajectories were assessed qualitatively for proximity to the ANT subregion target, using axial, coronal, sagittal, and lead trajectory plane static images. A novel method was devised to aid in defining the ANT in cases where visualization of anatomic landmarks (ie, AC, fornix, MTT) was difficult. The thalamus was segmented by defining the anterior-posterior (AP) and dorso-ventral (DV) axes at a parasagittal plane through the lead trajectory, and 4 quadrants of an ellipse created by outlining the thalamus using these major axes. When this parasagittal plane is centered on the junction of the MTT with the ventral border of the nucleus, the ANT occupies most of the anterior, superior quadrant and extends to, or just past the AP midpoint of the thalamus (Figure 1).

Lead locations were examined in all subjects for whom adequate postoperative imaging (n = 103) and 1-yr outcomes (n = 101) were available. Assessments of lead positions were made by 2 raters who were blinded to the outcome data. Each lead trajectory was assigned a score based on the following prospectively defined criteria: 3 = ideal placement, trajectory passes through the identified subregion target; 2 = slight deviation from ideal placement in one dimension (eg, posterior or medial) but still within a few millimeters of the target region; 1 = large deviation from ideal placement (either in multiple dimensions or in one dimension); 0 = trajectory did not appear to traverse the ANT. Representative examples of the range of lead placements (and scores) are shown in Figure 2.

Lead positions were assessed in sagittal, axial, and coronal images (in that hierarchy) and a total score assigned for each subject (range = 0-6 for bilateral placement). A score of 4 or greater was considered a good bilateral placement, indicating 2 trajectories near the target region. Scores below 4 were considered “suboptimal” as at least one lead would have been rated as deviating considerably from the “ideal” target. Lead placement scores were then compared to the clinical outcomes during year 1, defined as the average seizure reduction for 3 2-mo reporting periods during the unblinded phase (months 7-12). Because the lead placement scores were ordinal in nature (although they were described numerically) a categorical analysis (Fisher’s exact test) was conducted.

RESULTS

The original targeting analysis revealed that, despite marked variability, average active contact locations were comparable to the coordinates defined as the SANTÉ target (X = 5-6 mm, Y = 0-2 mm anterior to MCP, Z = 10-12 mm superior to the intercommissural plane) based on the Schaltenbrand and Wahren atlas. These coordinates represented the target for the center of the 3387 lead (ie, the interspace between contacts 1 and
FIGURE 2. Four examples of individual cases from the SANTÉ trial illustrating different lead trajectories and resultant placement scores. Each case includes 4 images: sagittal (S), coronal (C), axial (A), and probe’s eye (PE) trajectory views. Representative examples of ideal placement (R lead) score = 3 (top left); slight posterior placement (L lead) score = 2 (top right); very posterior placement (R lead) score = 1 (bottom left); and very medial placement (L lead) score = 1 (bottom right).

2). When compared to the clinical outcomes of the individual subjects, who were categorized as responders or nonresponders at 1-yr postimplant, there was no apparent relationship between active contact location and categorical outcome, with considerable overlap between the 2 groups (Figure 3).

In the new qualitative analysis of lead trajectory positions, individual scores for bilateral placements ranged from 1 to 6 across the subject cohort. Overall, out of 103 subjects, nearly 70% had a score of 4 or greater (good bilateral placement), with the most common deviations from the "ideal" target being in the medial and posterior directions (Tables 1 and 2).

The lead placement scores were mapped to each subject’s clinical outcome (% seizure reduction) during year 1 as shown in Figure 4, and assessed against the predefined categories for bilateral placement scores (good vs suboptimal) and clinical response (>50% reduction in seizures). These categorical outcome data are summarized in Table 3. Overall, it was found that subjects with a score of 4 or greater (ie, “good” bilateral placement) had a much higher probability of being a clinical responder than those with a score of 3 or less (43.5% vs 21.9%, P < .05, Fisher’s exact, 2-sided). When assessed across different subgroups based upon seizure onset location, this trend remained consistent (temporal onset: 50.0% vs 31.6%; extratemporal onset: 36.4% vs 7.7%) but was not significant due to the small sample sizes.

DISCUSSION

Accumulating evidence suggests that ANT DBS is an effective, durable therapy for partial onset epilepsy. The original evaluation of lead placements in the SANTÉ trial, done at the conclusion of the study, did not suggest a relationship between clinical outcomes...
and active contact location. This analysis was based on contact position in AC-PC stereotactic space and not on location relative to thalamic landmarks. Also, a relatively large number of leads (approximately 80%) were programmed with multiple cathodes.

To simplify the analysis, the position of the active contact in these cases was defined as the interpolation of the 2 contacts, based upon modeling of the stimulation fields. Given the relatively high stimulation amplitudes (typically 5-7.5 V) and use of multiple contacts on the 3387 lead (1.5 mm contact spacing), the volume

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### TABLE 1. Distribution of Bilateral Lead Placement Scores

| Bilateral score | Number of subjects (%) of subjects |
|-----------------|------------------------------------|
| 0               | 0                                  |
| 1               | 2 (1.9%)                           |
| 2               | 6 (5.8%)                           |
| 3               | 25 (24.3%)                         |
| 4               | 24 (23.3%)                         |
| 5               | 37 (35.9%)                         |
| 6               | 9 (8.7%)                           |

### TABLE 2. Direction of Individual Lead Placement Deviation From Ideal Target

| Lead placement deviation | Number of leads (%) of leads |
|--------------------------|-----------------------------|
| Lateral                  | 0 (0.0%)                    |
| Medial                   | 95 (46.1%)                  |
| Anterior                 | 5 (2.4%)                    |
| Posterior                | 53 (25.7%)                  |

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**FIGURE 3.** Results from the original coordinate-based analysis. Left panels show individual subjects’ active contact locations in the sagittal (top) and axial (bottom) planes for right (circles) and left (squares) leads with responders in blue and nonresponders in red (n = 94: responders = 43, nonresponders = 51). Right panels show median contact positions and one standard deviation from the median for both groups.
of tissue activated (VTA) was likely quite large in some of these subjects. In current practice of ANT DBS, it has become more common to use the Model 3389 lead (0.5 mm spacing) with initial stimulation voltages in the 2 to 3 V range on a single contact and titrate upward if needed, based on the size of this nucleus (similar to subthalamic nucleus (STN)) and modeling estimates of the resultant VTA.8

**TABLE 3. Distribution of Lead Placement Scores for Responders Versus Nonresponders**

| Bilateral scorea | Responder | Nonresponder |
|------------------|-----------|--------------|
| 3 or < (n = 33)  | 21.9%     | 78.1%        |
| 4 or > (n = 70)  | 43.5%     | 56.5%        |

*a A small group of subjects (n = 6) had bilateral scores of 4, with a score of 3 on one side and 1 on the other. Those subjects were evenly distributed between responders and nonresponders.

**Key Results**

In the current analysis, patients who had 2 well-placed leads, based upon their position within the target structure, had a much greater likelihood of being a clinical responder than those who did not, independent of seizure onset location. This result is consistent with experience in other DBS indications, where accurate lead placement at specific locations within the target nucleus is important and associated with better clinical outcomes.9 However, in this case, higher placement scores did not always favor being a responder. Therefore, good placement appears to be a necessary, but not sufficient, condition for success. Other, yet unknown, factors also likely influence individual patient outcome.

**Interpretation**

This new targeting analysis was motivated by recent studies examining lead location within the ANT, relative to specific landmarks (eg, MTT) and the relationship with clinical outcomes.3,7,10,11 Lehtimäki et al3 first identified a subregion in the anterior portion of the nucleus, superior to the MTT, which was associated with greater seizure reduction. The MTT is the main input to the ANT, and the outflow fibers from this structure exit via the anterior thalamic radiations in the lateral portion of the nucleus into the internal capsule.12 Stimulation of contacts in this target area therefore likely activates these densely packed axonal populations13,14 and, as in other DBS therapies, results in modulation of broader network activity, in this case in the Papez circuit. Based on the prior studies demonstrating a subregion within the ANT may be associated with superior efficacy, we evaluated the SANTÉ dataset in the context of lead trajectory relative to this target area. We a priori defined a rating/grading system that classified the lead trajectories relative to the ANT target region. Trajectories that were through or within a few millimeters of the target region were considered to be good placements given that the stimulation voltages used would likely capture this target region based upon VTA considerations. Trajectories that were more distant from this region were considered suboptimal. Our intent was to develop a methodology useful for evaluating ANT implantation, based on categorical methods, recognizing the variation that has been observed in the ANT DBS target. The fact that our results were in line with the findings from 4 prior, smaller studies was reassuring.

There was likely a learning curve for placement of DBS leads in this specific target during the SANTÉ trial as has been reported for other DBS therapies.15-17 Based on recent experience in a multicenter European study (MORE Registry), this DBS
Future, as a result of our study and those of others\textsuperscript{3,11,19} which
however, improved clinical outcomes may be attainable in the
experience using the same transventricular trajectory, and provide
from the SANTÈ trial are comparable to the MORE registry
contact resided somewhere within the ANT. The clinical results
not analyzed and replacement was not mandated so long as one
this criterion. However, quadrant or subregion within ANT was
randomized; 8.2\% of the leads needed to be revised based upon
criterion. However, quadrant or subregion within ANT was
not analyzed and replacement was not mandated so long as one
contact resided somewhere within the ANT. The clinical results
from the SANTÈ trial are comparable to the MORE registry
experience using the same transventricular trajectory, and provide
support for this approach versus the extraventricular trajectory,
even without specifically targeting the area superior to the MTT.
However, improved clinical outcomes may be attainable in the
future, as a result of our study and those of others\textsuperscript{3,11,19} which
appear to be converging on this target region as the most effective
stimulation site.

\textbf{Limitations}

The results presented here have clear limitations due to the
retrospective, post hoc nature. However, in the spirit of providing
information that can help to improve DBS therapy efficacy and to
benefit patients who elect to undergo the surgery and continued
follow-up associated with DBS, these results add information to the
knowledge base related to this therapy, which at this time
remains fairly limited.

\textbf{Generalizability}

It is universally accepted in movement disorders DBS that
accurate placement of leads into the STN, internal globus
pallidus, or ventral intermediate nucleus is critical for optimal
therapy efficacy. All of these therapies allow for evaluation of lead
location during surgery based on test stimulation results. Unfortu-
nately, for the ANT target, there are no reliable acute stimulation
induced positive effects, nor side effects, to help assess the position
of the leads. However, considering the growing body of evidence
related to targeting and clinical outcomes for this therapy, there
should be no reason to accept suboptimal lead placements given
the ability with current imaging technology to reliably evaluate
lead location either intra- or postoperatively. The significant
benefit observed during the SANTÈ trial, using widely spaced
electrode contacts and suboptimal targeting methods, suggests
an opportunity to improve outcomes with more accurate lead
placement.

\section*{CONCLUSION}

The results from this study suggest that a specific area within
the ANT, namely the anterior region, is associated with better
clinical outcomes with DBS. Subjects with good bilateral place-
ments in this target had a higher probability of being a clinical
responder (43.5\%) at 1 yr of follow-up, relative to the group
with a suboptimal placement (21.9\%). These findings from the
SANTÈ cohort are consistent with earlier reports from smaller
studies, and suggest that a certain degree of specificity in lead
targeting is critical for ensuring a good clinical outcome.

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COMMENTS

As with other DBS targets, it is logical that there may be a variation in response based on lead location, and it is intriguing that direct visualization of structural and anatomic features seemed to correlate better with outcome than traditional AC-PC targeting. However, while statistically significant, the post-hoc nature of the study and relatively small differences observed make it difficult to interpret how significant the effect might be. In addition, the definition of “ideal placement” relative to MTT is highly subjective (including descriptive judgement calls for “slight” vs. “large” displacement) and the definition of “good” placement as a score of 4 (which combines “slight” displacement on both sides with “large” displacement on one side) is somewhat arbitrary. If would have been much more compelling if the authors had used a more quantitative measure, such as identifying the putative target location in each subject and measuring distance of the active contacts from it. It is also worth noting that a majority of subjects in both groups were non-responders, and a number of subjects with “good” bilateral placement actually got worse. The data imply that targeting may indeed impact efficacy, but more evidence will be necessary to support the efficacy of this particular target.

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The authors present a thorough analysis of DBS electrode location within the anterior thalamic nucleus in >100 epilepsy patients who were monitored for degree of symptomatic improvement for more than a year after the implant. Not surprisingly, precise targeting was associated with remarkably higher chance of meaningful clinical response with almost 2-fold difference between those with optimal and suboptimal location of stimulating contacts.

To further improve individual outcomes, one will need to develop either an easily identifiable set of radiographic landmarks, or a reliable neurophysiological indicator of the target. Alternatively, one may use technological advancement in electrode leads (directional, segmented, etc) to compensate for inaccurate targeting.

It would be interesting to extend this analysis to hundreds of patients implanted with ANT DBS outside of SANTÉ trial to see if the authors’ findings are indeed valid.

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