The effectiveness of an actuator-driven pulsed water jet for the removal of artificial dental calculus: a preliminary study

Yuka Sato, Masahiro Iikubo*, Takashi Nishioka, Nobuhiro Yoda, Tetsuya Kusunoki, Atsuhiro Nakagawa, Keiichi Sasaki and Teiji Tominaga

Abstract

Background: While hand and ultrasonic scalers are the primary tools used for the removal of dental calculus in periodontal treatment, many studies have shown that they also damage the enamel surface. We have developed a novel actuator-driven pulsed water jet (ADPJ) system, which has the ability to selectively remove materials depending on their stiffness. Considering the different material properties between teeth and dental calculus, it might be possible to develop the ADPJ to remove dental calculus without damage to the tooth’s enamel surface using a suitable jet pressure. Therefore, the aim of this study was to assess the effectiveness of the ADPJ in removing dental calculus, and the surface features of the teeth after its use.

Methods: A total of 93 artificial teeth coated with artificial dental calculus were examined in this study. The weights of 90 teeth were measured before and after the use of ADPJ, which had an applied voltage setting of 150, 200, or 240 V. The three remaining teeth were instrumented with a conventional hand scaler, ultrasonic scaler, or ADPJ (set at 240 V). Damage to the artificial tooth surfaces was evaluated using 5% Evans blue dye under an optical microscope. Furthermore, apatite pellets, which are utilized as experimental substitutes for natural teeth, were assessed after the use of ADPJ and both conventional scalers.

Results: The ADPJ significantly reduced the amount of artificial calculus, and the removal rate was dependent on the applied voltage. No damage was observed on the surface of the artificial tooth and apatite pellet following the use of ADPJ, in contrast to the conventional scalers.

Conclusions: The results of this study demonstrate the in vitro effectiveness of ADPJ in the removal of dental calculus, without causing damage to tooth surfaces.

Keywords: Actuator-driven pulsed water jet, Dental calculus, Tooth surface

© The Author(s). 2020 Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article’s Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article’s Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/. The Creative Commons Public Domain Dedication waiver (http://creativecommons.org/publicdomain/zero/1.0/) applies to the data made available in this article, unless otherwise stated in a credit line to the data.
**Background**

Dental calculus is formed supra- and sub-gingivally, and contributes to the irritation and inflammation of the gingiva; this in turn leads to gingivitis and periodontitis. Removal of dental calculus is the mainstay of prevention and treatment of periodontal disease [1], and this is most commonly accomplished with the use of ultrasonic or hand scalers [2]. Especially, ultrasonic scalers are often used, owing to their simplicity, efficiency, and the wide range of designs available for accessing different anatomical areas. However, many studies have reported that both ultrasonic and hand scalers cause damage to the enamel surface, especially the ultrasonic scaler makes deep damage on the crack line of the enamel surface and crater formation with remarkable disintegration of the demineralized enamel surface [3, 4]. Some studies have reported the use of an erbium-doped yttrium aluminum garnet laser (Er: YAG laser) with high pulse repetition rates (focused on a small area) to selectively remove dental calculus with high precision [5–7], with limited damage to the sound tissues [6, 7]. Nevertheless, the guideline has stated that the use of lasers to remove dental calculus is contraindicated due to the risk of thermal damage and ablation of enamel [6]. Therefore, the development of a device that can safely remove dental calculus without damaging the enamel surface is required.

We have previously developed an actuator-driven pulsed water jet (ADPJ) system which removes lesions, such as tumors, with minimal damage to the surrounding healthy tissues [8]. The ADPJ is an emerging technology with a remarkably reduced water consumption and has the ability to selectively remove tissues based on their material stiffness [8–10]. Considering the different material properties of enamel and dental calculus, it might be possible to develop the ADPJ to use appropriate water pressure to remove dental calculus without damaging the underlying enamel surface. Since the water pressure of the ADPJ was consistently and positively correlated with the applied voltage [9, 10], we subsequently modified our original ADPJ and developed a device with a higher applied voltage, with the aim of removing harder materials such as dental calculus. The objective of this study was to assess the effectiveness of this modified ADPJ system at different applied voltage settings, in removing dental calculus using an artificial model. Furthermore, we assessed the ability of the ADPJ to limit damage to enamel surfaces, in comparison to conventional scalers.

**Methods**

**ADPJ system**

We have previously described the mechanism of the ADPJ system [8–10]. In brief, this system is composed of a pump chamber driven by a piezo-actuator, a stainless steel tube, and a nozzle with an internal diameter of 0.15 mm, as shown in Fig. 1. Pure water is continuously fed into a chamber that supplies the water pump through a capillary inlet (inner diameter, 0.3 mm) at a flow rate of 12.4 mL/min. The piston driven by the piezo-actuator compression occurs from 0 to 125 μs after a sinusoidal wave pattern with a phase angle of $-\pi/2$ to $\pi/2$. Piston recovery occurs gradually from 125 to

![Fig. 1 Schematic diagram (a) and photograph (b) of the piezo ADPJ system. The ADPJ is generated by the movement of piston driven, the water is released through the chamber continuously. The three-dimensional water flow ejected from the nozzle can be adjusted with a manual switch, and the water volume and speed are easy to control. Dissected tissue and splashed and excess liquid are aspirated through the removable silicone suction tube connected to a conventional aspirating system in the operating theater. ADPJ: actuator-driven pulsed water jet, CP: stainless steel connecting pipe, Di: stainless steel diaphragm, PA: piezo electric actuator](image)
5000 μs after a low-frequency sinusoidal wave pattern. The resultant piston is moved at a frequency of 200 Hz. The piston pushes the diaphragm forward to compress the chamber and generates pressure. The elevated pressure in the chamber propagates to the nozzle through the connecting pipe. Water ejected from the nozzle can be removed through the suction tube.

In our previous ADPJ system, the peak-to-peak value of the applied voltage that drove the piston was set at 5 to 100 V \([8–10]\). In this experiment, the maximum voltage was increased to 240 V, with the aim of removing dental calculus, which is stiffer than the previously tested materials.

**Mechanical properties of the water jet**

The mechanical properties of the ADPJ system were evaluated by measuring the peak pressure with a cavity-mounted pressure sensor (Quartz High-Pressure Sensor, Model 601A; Kistler Instrumente AG, Winterthur, Switzerland). The length of the sensing hole was 0.5 mm and the diameter was 0.15 mm, which was equivalent to that of the nozzle diameter of our ADPJ system. The sensing hole was tapered and connected to the cavity \((1.5 \text{ mm length})\), which had the same diameter as the pressure sensor. The nozzle of the ADPJ system was placed 0.5 mm from the sensing hole and the pressure was measured accordingly. The tip of the cavity-mounted pressure sensor unit and the ADPJ system was placed in a water reservoir from which air was extracted to avoid the formation of bubbles. The peak pressure of the ADPJ was measured three times for each applied voltage setting \((150 \text{ V, } 200 \text{ V and } 240 \text{ V})\).

**Preparation of the dental calculus samples**

Before the experiment, the weight of each artificial tooth (initial weight) was measured using a standard-level precision balance \((FX-300i, \text{ Kensei Kogyo Co., Ltd., Ibaraki, Japan})\). As shown in Fig. 2a, the artificial dental calculus \((\text{Dental Calculus Set; Nisshin Dental Products Inc., Tokyo, Japan})\) was coated over the entire surface of each artificial right upper primary incisor crown \((n = 93)\) \((\text{Invictus, A-PRO3A; Nisshin Dental Products Inc., Tokyo, Japan})\) with a uniform thickness. The teeth were stored for over 24 h in a controlled environment at 24 °C before being subjected to the ADPJ.

**Evaluation of the effectiveness of artificial dental calculus removal**

After the weights of the samples \((\text{weight before ADPJ})\) were measured, the artificial dental calculus was removed with the ADPJ system set at a voltage of either 150 V, 200 V, or 240 V, and for a duration of either 10 s, 20 s, or 30 s. Ten trials, in which the nozzle of ADPJ was placed perpendicular to the artificial dental calculus, at a distance of approximately 1.5 mm, and ran in parallel to the artificial tooth surface, were performed for each combination of treatment duration and applied voltage setting, for a total of 90 trials. The weight of each artificial tooth \((\text{weight after ADPJ})\) was measured again after a period of at least 24 h in a controlled environment at 24 °C. The removal rate \((\%)\) of the artificial dental calculus was analyzed based on the following formula: \((\text{weight before ADPJ} - \text{weight after ADPJ}) \times 100 / (\text{weight before ADPJ} - \text{initial weight})\).

**Evaluation of the surface of the artificial teeth and apatite pellets**

The artificial dental calculus of three samples was removed by either a conventional hand scaler \((\text{No.23326 G6, YDM Co., Tokyo, Japan})\), ultrasonic scaler \((\text{0E5, NSK Ltd., Tokyo, Japan})\), or ADPJ \((\text{set at } 240 \text{ V})\) for 1 min. The conventional hand scaler and ultrasonic scalers were used by a dentist with more than 20 years of experience. The artificial teeth were immersed in 5% Evans blue dye solution for 10 s, and
rinsed with water for another 10 s. The buccal surfaces of the artificial teeth were evaluated under an optical microscope (TG500PC, Shodensha, Inc., Osaka, Japan).

Apatite pellets (APP-100; 10 × 10 × 2 mm, Hoya Technosurgical Co., Tokyo, Japan), which are utilized as experimental substitutes for natural teeth in studies investigating the abrasiveness of toothbrushes and tooth paste, were polished in one direction to evaluate the surface properties; they were then attached to a stage moved in a direction perpendicular to that in which they were polished (EZSM 3E020-K, Oriental Motor Co., LTD, Tokyo, Japan) [11]. The nozzle of the ADPJ was placed 1.5 mm from the apatite pellet, and the applied voltage was set to 240 V. The apatite pellet was subsequently moved 10 mm at a speed of 0.5 mm/s. Ultrasonic and hand scalers were pressed against the apatite pellet with a force of 0.4 N, 0.6 N or 0.8 N; this was performed after both scalers were placed on an electronic balance and the pressure was adjusted [12]. The scratch on the apatite pellet surface was evaluated by laser microscopy (VK-9500, Keyence Co., Inc., Osaka, Japan).

Statistical analysis
All values are presented as means ± standard error. Statistical analyses were performed using JMP 13 Pro statistical software (SAS Institute Inc., Cary, NC, USA). Comparisons of the nine groups were performed using a one-way analysis of variance test and Tukey-Kramer HSD test. The level of statistical significance was set at \( p < 0.05 \).

Results
The effectiveness of artificial calculus removal with ADPJ under each condition
As shown in Fig. 3, the peak pressure of the pulsed water jet was positively correlated with the applied voltage \( (R^2 = 0.9943, p < 0.001) \).

The mean adherent weight of the artificial dental calculus (weight before ADPJ – initial weight) was 22.2 ± 6.8 mg and there was no significant intergroup difference. Figure 2b depicts typical samples of artificial teeth after ADPJ treatment under the three applied voltage settings (150 V, 200 V, and 240 V) and three treatment durations (10 s, 20 s, and 30 s). The artificial dental calculus was partially removed from the surface of the artificial tooth, and the extent of removal was dependent on the applied voltage setting and duration of the treatment.

Figure 4 presents the results of the comparisons in the mean artificial dental calculus removal rate, between the different combinations of the applied voltage settings and treatment durations. The removal rate was found to be highly dependent on both the applied voltage setting and treatment duration. In a comparison between treatment durations at a constant applied voltage setting of 200 V or 240 V, a 30 s treatment duration resulted in a significantly greater removal rate than those of 10 s and 20 s. At a constant applied voltage setting of 150 V, a significant difference was only observed between a treatment duration of 30 s versus 10 s. Among the comparisons between applied voltage settings with a constant treatment duration of 20 s, a significantly higher removal rate was observed for 240 V compared to 150 V. Similarly, at a constant treatment duration of 30 s, the removal rate was significantly greater for 240 V compared to 150 V (all \( p < 0.05 \)).

Surface of the artificial teeth and apatite pellets
As shown in Fig. 5a, the Evans blue dye was not visible on the surface of the artificial tooth treated with ADPJ. In contrast, it was clearly retained on the surfaces of the artificial teeth treated with the hand (Fig. 5b) and ultrasonic scalers (Fig. 5c).
Figure 6 shows that the laser microscopic images of the surfaces of apatite pellets after treatment with the ADPJ, hand scaler and ultrasonic scaler. A scratch mark was not observed on the surface of the apatite pellets after ADPJ treatment (Fig. 6a). In contrast, a vertical scratch mark was observed after the use of both the hand (Fig. 6b) and the ultrasonic scalers (Fig. 6c).

Discussion

The aim of this study was to test the hypothesis that the ADPJ could remove dental calculus without damaging the underlying enamel surface. The use of artificial teeth and dental calculus facilitated the standardization of experimental variables between groups, as the level of existing calculus is widely variable on natural teeth. Indeed, Sawaguchi et al. [12] reported that the removal force variation was smaller in the artificial than the natural dental calculus adhered to the artificial and human teeth, respectively.

In the first phase of this study, we developed a high-voltage ADPJ with a maximum setting of 240 V; this was modified from our previous device, which was designed to remove lesions on soft tissues (e.g., liver; 40–80 V, internal thoracic artery; 80–100 V) [9, 10]. We demonstrated that the effectiveness of dental calculus removal by the ADPJ at a constant jet pressure was dependent on the applied voltage (Fig. 3), and that a high voltage ADPJ would be required for periodontal treatment in a clinical setting. Previous studies have reported that the cutting ability and speed of a pulsed jet on harder materials is greater compared with the continuous jet operating at the same parameters (i.e., nozzle diameter, operating pressure, and output power) [13]. These findings may explain why a pulsed water jet can efficiently dissect tissues with a relatively smaller amount of water and energy. It is possible that accumulated water on the tissue surface affects the dissecting ability, and it is necessary to study this effect in the future. It has previously been shown that water released from the tip of the ADPJ can remove a tumorous lesion, while leaving the surrounding normal tissues unharmed [14]. The results of the present study suggest that it is possible for the pulsed water flow to penetrate and accumulate in between the artificial tooth surface and the attached artificial calculus, and effectively dislodge the latter.

In order to evaluate damage to the tooth surface, both artificial teeth and apatite pellets were used. The rationale
The results of this study suggest that the ADPJ may be used safely for the removal of calculus. There are some limitations to this study. First, the effectiveness of the ADPJ in removing natural dental calculus is not clear, as we have used an artificial model in this study. Considering the different material properties between the artificial and natural dental calculus, further studies will be needed to evaluate ADPJ effectiveness on natural teeth. In addition, the use of high-voltage ADPJ for the removal of calculus adjacent to soft tissues (e.g., in the case of subgingival calculus adhered to the tooth root surface) requires additional safety evaluations. Prior to clinical use, it is necessary to determine the effect of applying a high voltage to the soft tissues and tooth root surfaces at various nozzle positions, distances, and angles in animal experiments. The observation of root surface damage or soft tissue damage (i.e., bleeding or inflammation) would necessitate a readjustment of the applied voltage, frequency, and water volume. Furthermore, long-term clinical studies comparing the prognosis of treated teeth after the use of ADPJ and conventional scalers are required to substantiate the clinical effectiveness of the pulsed water jet system.

**Conclusions**

We evaluated the effectiveness of the ADPJ in removing artificial dental calculus as well as the surface features of artificial teeth and apatite pellets. The results of this study demonstrated the ability of the ADPJ to remove artificial dental calculus without damage to the surface of artificial teeth and apatite pellets. Further studies on calculus adhered to natural teeth are required to substantiate the clinical effectiveness of the ADPJ, and its potential to be integrated into routine periodontal therapy.

**Abbreviations**

ADPJ: Actuator-driven pulsed water jet; Er:YAG laser: Erbium-doped yttrium aluminum garnet laser; CP: Stainless steel connecting pipe; Di: Stainless steel diaphragm; PA: Piezo electric actuator

**Acknowledgements**

We would like to thank Editage (www.editage.com) for English language editing. We are also obliged to Seiko Epson Corporation for preparing the ADPJ. We would like to acknowledge Ms. Emiko Kaneda, Ms. Kyoko Sugai, Ms. Chiho Sato for their administrative assistance.
Authors’ contributions
Concept/design: Y Sato, M Iikubo, T Nishioka, N Yoda, and A Nakagawa. Data analysis/interpretation: M Iikubo, K Sasaki, and T Tominaga. Data acquisition: Y Sato, T Nishioka, N Yoda, T Kusunoki, and A Nakagawa. Statistics: M Iikubo. Draft of the article: Y Sato, M Iikubo, T Nishioka, N Yoda, and T Kusunoki. Critical revision of the article: A Nakagawa, K Sasaki, and T Tominaga. Approval of the submitted and final version: all authors.

Funding
This investigation was supported in part by a Grant-in-Aid for Scientific Research (A) (No. 18H04157) and Challenging Exploratory Research (No. 16 K15810) from the Japanese Ministry of Education, Culture, Sports Science and Technology (MEXT).

Availability of data and materials
The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

Ethics approval and consent to participate
Not applicable.

Consent for publication
Not applicable.

Competing interests
The ADPJ device was a free rental from Seiko Epson Corporation under a collaborative research contract with Tohoku University, to Y.S., M.I., and A.N.

Author details
1Division of Dental Informatics and Radiology, Tohoku University Graduate School of Dentistry, 4-1 Seiryo-machi, Aoba-ku, Sendai, Miyagi 980-8575, Japan. 2Division of Advanced Prosthetic Dentistry, Tohoku University Graduate School of Dentistry, Sendai, Miyagi, Japan. 3Department of Neurosurgery, Tohoku University Graduate School of Medicine, Sendai, Miyagi, Japan.

Received: 17 April 2020 Accepted: 3 July 2020

Published online: 13 July 2020

References
1. Rameezer CA, Anerud A, Dulac M, Lulic M, Cullinan MP, Seymour GI, et al. Natural history of periodontitis: disease progression and tooth loss over 40 years. J Clin Periodontol. 2017;44(12):1182–91.
2. Walmsley AD, Lea SC, Landini G, Moses AJ. Advances in power driven pocket / root instrumentation. J Clin Periodontol. 2008;35(8 Suppl):22–8.
3. Lea SC, Felver B, Landini G, Walmsley AD. Ultrasonic Scaler oscillations and tooth-surface defects. J Dent Res. 2009;88(3):229–34.
4. Kim SY, Kang MK, Kang SM, Kim HE. Effects of ultrasonic instrumentation on enamel surfaces with various defects. Int J Dent Hyg. 2018;16(2):219–24.
5. Aoki A, Ishikawa I. The application of Er:YAG laser for removal of calculus. Shika J. 1994;39(3):279–87 (in Japanese).
6. Japanese Society for Laser Dentistry. Safety guidelines for the laser removal of dental calculus. Laser Ther. 2012;21(2):137–45.
7. Fried WA, Chan KH, Darling GL, Fried D. Selective removal of dental calculus with a diode-pumped Er:YAG laser. ProcSPIE Int Soc Opt Eng. 2019;10857:108570M.
8. Seto T, Yamamoto H, Takayama K, Nakagawa A, Tominaga T. Characteristics of an actuator-driven pulsed water jet generator to dissecting soft tissue. Rev Sci Instrum. 2019;82(3):035105.
9. Yamada M, Nakano T, Sato C, Nakagawa A, Fujishima F, Kagawishii N, et al. The dissection profile and mechanism of tissue-selective dissection of the piezo actuator-driven pulsed water jet as a surgical instrument: laboratory investigation using swine liver. Eur Surg Res. 2014;53(1–4):61–72.
10. Suzuki T, Kawamoto S, Nakagawa A, Endo T, Tominaga T, Akiyama M, et al. Application of actuator-driven pulsed water jet for coronary artery bypass grafting; assessment in a swine model. J Artif Organs. 2018;21(2):247–53.
11. Tanaka A, Tomiyama K, Ohashi K, Miyake K, Shimizu T, Hamada N, et al. Relevance of surface characteristics in the adhesiveness of polymicrobial biofilms to crown restoration materials. J Oral Sci. 2018;60(1):129–36.
12. Sawaguchi M. A study on the removal force of standardized models with artificial calculus. J Japanese Soc Periodontol. 2006;48(4):267–75.
13. Foldyna J, Stek L, Svehla B, Svehla S. Utilization of ultrasound to enhance high-speed water jet effects. Ultrason Sonochem. 2004;11(3–4):131–7.
14. Nakayashiki A, Kawaiuchi T, Nakagawa A, Sato M, Moctizuki F, Endo T, Tominaga T. Water veil effect to control splashing from the pulsed water jet device: minimizing the potential risk of dissemination using surgical aspirators. J Neurol Surg A Cent Eur Neurosurg. 2018;79(4):309–15.

Publisher’s Note
Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.