Magnetic resonance diffusion-weighted imaging in diagnostics of primary fallopian tube carcinoma – is it useful?

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Abstract

Purpose: Primary fallopian tube carcinoma (PFTC) is the rarest form of female genital malignancy. The imaging applied for suspected adnexal masses includes transvaginal ultrasound (US), computed tomography (CT), and magnetic resonance imaging (MRI), but the vast majority of PFTC is recognised intraoperatively.

Material and methods: The study group consisted of seven women with postoperatively histopathological diagnosis of PFTC. To recognise characteristic findings for PFTC, retrospective analysis of preoperative MRI was performed. All patients underwent MRI of the pelvis and abdomen using a 1.5T MR system. Based on the results of the above imaging, suspected adnexal masses were recognised. MRI protocol contained T2-weighted images, fat-suppressed T2-weighted, T2-TIRM, DW EPI, pre- and postcontrast dynamic 3D T1 GRE in transverse orientation, with diffusion weightings of 0, 50, 100, 150, 200, 400, 800, and 1200 s/mm². Regions of interest were outlined by a radiologist, who documented the character of adnexal masses on diffusion-weighted (DW) images and apparent diffusion coefficient (ADC) maps.

Results: In all seven patients with PFTC unilateral tumour was found. On all DW images (with $b$ values of 0, 50, 100, 150, 200, 400, 800, and 1200 s/mm²) the mean signal intensities of solid parts of tumour were significantly higher than the mean signal intensities of normal ovarian tissue ($p=0.0001$). There were no statistically significant differences between eight $b$ values applied for ADC calculations.

Conclusions: Preoperative diagnostics of PFTC is difficult and mainly based on morphological features. Previous research did not show characteristics of PFTC in post-contrast dynamic imaging. In our material a clear increasing of signal intensity in DW imaging occurred independently of the $b$ value.

Key words: primary fallopian tube carcinoma (PFTC), magnetic resonance diffusion-weighted imaging, ADC values of fallopian tube tumours.

Introduction

Primary fallopian tube carcinoma (PFTC) is the rarest form of female genital malignancy. Its frequency is estimated to be less than 1-2%. It is mostly diagnosed in the period from the fourth to sixth decade of life [1,2]. The germ-line BRCA1 and BRCA2 mutations are the only documented risk factors related to its aetiology. Some papers have described the theory that high-grade serous ovarian carcinoma and peritoneal carcinoma may originate from occult high-grade serous carcinoma in the fallopian tubes [3,4]. Diagnostics carried out for suspected adnexal masses includes transvaginal ultrasound, computed tomography (CT), and magnetic resonance imaging (MRI) of the pelvis and abdomen, but the vast majority of PFTC are recognised intraoperatively. The treatment of PFTC is based on debulking surgery and adjuvant platinum-based chemotherapy, similar to ovarian cancer [5,6].
MR imaging is the established modality for the diagnosis of adnexal malignancies. This technique can also be used to determine the source or extension of disease. Advances in MRI technology, including improvement of diffusion-weighted imaging technique (DW imaging), could increase the sensitivity of MRI for differentiating tumours of the fallopian tube and ovary, especially in the early stages. Previous studies have shown the efficacy of DW images to detect different pelvic malignancies, e.g. ovarian [7]. There is lack of standardisation of DW image acquisition (choice of different b values) and calculation of the apparent diffusion coefficient (ADC).

The aim of this study was to assess the accuracy of DW imaging for the detection of PFTC in patients with suspected adnexal masses, and to evaluate ADC values of fallopian tube tumours.

Material and methods

The study group consisted of seven women aged from 48 to 69 years with postoperative histopathologic diagnosis of PFTC. In all cases serous high-grade carcinomas were confirmed. According the FIGO staging, four patients were at stage I, one at stage II, and two at stage III of PFTC. To recognise characteristic findings for PFTC the retrospective analysis of preoperative MR imaging was performed.

Magnetic resonance imaging

The group of patients underwent MR imaging of the abdomen and pelvis at our MR Lab. All MR imaging was performed with a 1.5 T clinical whole-body MR system (MAGNETOM Avanto; Siemens AG, Erlangen) using the Spine Matrix coil for full coverage of the abdomen and pelvis. Based on the results of the above imaging, suspected adnexal masses were recognised.

MRI protocol for the detection of the abdominal and pelvic lesions consisted of turbo spin-echo (TSE) T2-weighted images, fat-suppressed T2-weighted, T2-TIRM, DW EPI, pre- and post-contrast dynamic 3D T1 GRE in transverse orientation. The most imported of the applied parameters of MR imaging are shown in Table 1. Pelvic axial DW images were acquired using the same multi-slice EPI sequence for all cases: 30 × 6 mm slices; 380 × 380 mm FOV; 128 × 96 matrix; TR = 3800 ms; TE = 73 ms; with diffusion weightings of 0, 50, 100, 150, 200, 400, 800, and 1200 s/mm².

Gadobutrol (Gadovist, Bayer Schering) was administered at a dose of 0.1 ml/kg, immediately followed by a bolus of 20 ml of 0.9% NaCl.

Image analysis

Regions of interest (ROI) were outlined in a Multi-Modality Workplace Station (Siemens Medical Solution) by a radiologist with experience in pelvic MR imaging, who documented the character of adnexal masses on DW images and ADC maps.

Subsequently, freehand ROI were drawn on the ADC and all b value images by using the T2-weighted images for guidance. ROI included as large a part of the solid lesion as possible, avoiding areas of necrosis, partial volume effect, and artefacts. ROI was copied and pasted from DW image to proper ADC map. The measurements on the ADC map were recorded. ADC was measured twice for

| Table 1. Parameters of applied magnetic resonance sequences |
|-----------------|-----------------|-----------------|-----------------|
| Parameter       | T2 TSE          | T2 TSE; Fat-Sat | DW EPI          | T2 TIRM         | 3D T1 GRE       |
| Repetition time (ms) | 4250            | 2110            | 3800            | 6100            | 3.05            |
| Echo time (ms)   | 117             | 123             | 73              | 39              | 1.13            |
| Flip angle (deg.)| 137             | 150             | 90              | 150             | 10              |
| Turbo factor     | 51              | 51              | –               | 9               | –               |
| EPI factor       | –               | –               | 96              | –               | –               |
| iPAT factor      | –               | 2               | 2               | –               | 2               |
| Plane            | Axial           | Axial           | Axial           | Axial           |
| Number of signal averages | 1             | 1               | 4               | 1               | 1               |
| FOV (mm)         | 360             | 360             | 360             | 360             | 360             |
| Rectangular FOV (%) | 75             | 100             | 75              | 75              | 75              |
| Matrix           | 384 × 512       | 256 × 256       | 96 × 128        | 288 × 384       | 156 × 288       |
| Slice thickness (mm) | 5              | 5               | 6               | 5               | 3               |
| Respiratory triggering | No             | Yes             | No              | No              | No              |
| Breath-hold      | No              | Yes             | No              | No              | No              |

EPI – echo-planar imaging, FOV – field of view

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Figure 1. Primary fallopian tube carcinoma. Axial T1-weight fat-sat magnetic resonance imaging. The moderate and heterogenous enhancement of solid parts of the tumour (arrows).

Figure 2. Primary fallopian tube carcinoma. Patient 1. Diffusion-weighted imaging b 100 s/mm². The part of the solid tumour of fallopian tube with high signal intensity (arrow).

Figure 3. Primary fallopian tube carcinoma. Patient 2. Diffusion-weighted imaging b 100 s/mm². The part of the solid tumour of fallopian tube with high signal intensity (arrow).

Figure 4. Primary fallopian tube carcinoma. Patient 1. Diffusion-weighted imaging b 800 s/mm². The part of the solid tumour of fallopian tube with high signal intensity (arrow).

Figure 5. Primary fallopian tube carcinoma. Patient 2. Diffusion-weighted imaging b 800 s/mm². The part of the solid tumour of fallopian tube with high signal intensity (arrow).

Figure 6. Primary fallopian tube carcinoma. Patient 1. Diffusion-weighted imaging b 1200 s/mm². The part of the solid tumour of fallopian tube with high signal intensity (arrow).
ADC values were calculated by mono-exponential regression with the following formula: $S = S_0 \times \exp(-b \times DC)$, where $S$ is the signal intensity after application of the diffusion gradient, and $S_0$ is the signal intensity at $b = 0$ s/mm$^2$. Eight $b$ values were applied for ADC calculation.

**Statistical analysis**

All statistical analyses were performed using the STATISTICA v.12 (Statsoft, Tulsa, USA) software package. Comparisons of mean ADC and mean $b$-value images ($b$ 50, 100, 150, 200, 400, 800, 1200 s/mm$^2$) between solid parts of fallopian tube tumour and normal ovarian tissue were analysed using an unpaired two-tailed $t$-test; $p < 0.05$ indicated a statistically significant difference.

**Results**

In all seven patients with PTFC unilateral tumour was found. The largest tumour diameter ranged from 18 mm to 130 mm. MRI shown a sausage-like shape tumour in five patients (71%) and irregular polycystic lesion in two cases (29%). The signal the solid parts of the fallopian tube tumour was homogenous and hyperintense in T2-weighted images and demonstrated enhancement on T1-weighted images in all patients (Figure 1).

On all DW images (with $b$ values of 0, 50, 100, 150, 200, 400, 800, and 1200 s/mm$^2$) the mean signal intensities of solid parts of tumour were significantly higher than the mean signal intensities of normal ovarian tissue ($p = 0.0001$) (Figures 2-7). Mean ADC values of tumour tissue were significantly lower than those of reference ovary ($p = 0.0001$). There were no statistically significant differences between the eight $b$ values applied for ADC calculations (Figures 8 and 9).

In three patients in FIGO stage II and III extratumoural lesions were found on DW-images (peritoneal and omental implants).

**Discussion**

PFTC represent less than 1% of all female genital malignancies. Pathology remains the mainstay for diagnosis of PFTC. Serous carcinoma is the most common histological type of tubal cancer. These tumours are identical to their ovarian counterparts [1].

Clinically it resembles ovarian cancer, and ovarian tumour is the usual preoperative recognition. The tubal carcinoma is rarely recognised preoperatively and is usually first appreciated during the operation or by a pathologist [5,6].

Due to its very rare occurrence, previous original reports of diagnosis of PFTC relate to groups from a few to a dozen patients. Imaging routinely carried out for suspected adnexal masses includes transvaginal ultrasound, CT scan, and MR imaging of the abdomen and pelvis. The appearance of PFTC can be characteristic: an adnexal...
tubular cystic structure, representing hydrosalpinx, and containing papillary projections or solid mural nodule [8].

MR imaging is particularly helpful in the initial evaluation of adnexal malignancies, due to its multiplanar capability with superior soft tissue contrast. Until now the differential diagnosis in MRI was based on morphological feature as a typical small sausage-like solid unilateral mass. On MRI hydrosalpinx appears as simple serous fluid, homogeneously hyperintense on T2-weighted images and hypointense on T1-weighted images [8]. We obtained these results in our group. If protein or haemorrhagic fluid is present, it appears heterogeneously hyperintense on T2-weighted images and hypointense on T1-weighted images. The solid tumour component of PFTC is homogeneously or heterogeneously iso- or hyperintense on T2-weighted images, hypointense on T1-weighted images, and demonstrates enhancement [9,10]. In some papers the authors suggest that the enhancement of solid parts is mild to moderate, heterogeneous, and uncharacteristic [11,12]. However, the diagnosis is still based on morphological features.

We tried to find specific features of PFTC in DW imaging. On our exams (with b values of 0, 50, 100, 150, 200, 400, 800, and 1200 s/mm²) the diffusion restriction of solid parts of the tumour were significantly higher than the mean signal intensities of normal ovarian tissue (p = 0.0001). There is no border b value specific to PFTC. It is the different PFCT from the ovarian carcinoma, where the most ovarian malignancies show diffusion restriction at high b levels (> 300) [13,14].

The small number of patients is an important limitation of this study, but we must take into account that PFTC is a very rare tumour. However, our results should be regarded as preliminary in terms of sensitivity and specificity of DW imaging for the differential diagnosis of PFTC and should be confirmed in a multicentre study.

Conclusions
Preoperative diagnostics of PFTC is difficult and is based mainly on morphological features. Previous research did not show characteristics of PFTC in post-contrast dynamic imaging. In our material a clear increase in signal intensity in DW imaging occurs independently of the b value.

Conflict of interest
The authors report no conflict of interest.

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