Lactic acid modified rare earth-based nanomaterials for enhanced radiation therapy by disturbing the glycolysis

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Abstract
Deficient deposition of X-rays and strong capacity of repairing damage DNA of cancer cells limit the effect of radiation therapy (RT). Herein, we synthesize CsLu2F7 nanoparticles with lactic acid (LA) ligands (CsLu2F7-LA) to overcome these limitations. The high-Z atoms of Lu and Cs can deposit more X-rays for generating enhanced hydroxyl radicals (·OH). Meanwhile, the LA ligand will guide CsLu2F7-LA to target monocarboxylic acid transporter (MCT) and impede the transportation of free LA, leading to decreased glycolysis and DNA damage repair. Consequently, the curative effect of RT will be enhanced and the strategy of LA accumulation induced radiosensitization is proved by in vivo and in vitro experiments, which will bring prospects for enhanced RT with nanomedicine.

Keywords: Nanomedicine, Rare earth, Radiation therapy, Lactic acid, Glycolysis

Background
Radiation therapy (RT) is widely used in clinic for the treatments of cancer [1–3]. According to the statistics, nearly 60% of the cancer patients need RT in the treatment plans [4]. In the process of RT, X-ray will decompose water molecules (H2O) to generate reactive oxygen species (ROS), mainly hydroxyl radicals (·OH). Generally, ·OH will attack DNA molecules, induce irreversible DNA double-strand breaks (DSBs), and finally lead to the proliferative death of cancer cells [5, 6]. Unfortunately, there are still some obstacles limit the curative effect of RT. Firstly, biological tissues mainly consist of low-Z atoms such as C, H, O, N, P and S, which can deposit few X-rays and result in deficient yield of ·OH [7, 8]. Secondly, cancer cells will devote themselves to repairing the damage caused by RT [9–12]. For example, cancer cells will enhance the metabolism to synthesize enough lipids and proteins to replace the damaged organelles [9, 13]. Hence, it is necessary to develop new methods for increasing the deposition of X-rays and decreasing the metabolism of cancer cells in RT, simultaneously.

Recently, the progress of nanomedicine brings more chances for radiosensitization [14–21]. On the one side, a series of nanomaterials containing high-Z atoms including Lu, Hf, Ta, Au and Bi have been developed for increasing the deposition of X-rays [22–29]. On the other side, the metabolism of cancer cells depends on aerobic glycolysis, which is also called Warburg Effect [30, 31]. Inhibiting the process of glycolysis has much potential for enhancing the effect of cancer therapy [32]. Some small molecules have been developed for inhibiting critical enzymes including hexokinase, pyruvate dehydrogenase and lactate dehydrogenase in the process of glycolysis. In addition, these inhibitors have shown further synergistic effect with RT or chemotherapy [33–36]. Hence,
developing high-Z nanomaterials with the ability of disturbing glycolysis will present a satisfactory performance for radiosensitization.

Lactic acid (LA) is the final product in the process of glycolysis and plays an important role in tumor progression [37]. Cancer cells will generate a mass of LA and excrete them to tumor microenvironment (TME) through monocarboxylic acid transporter (MCT) [38, 39]. The accumulation of LA will decelerate glycolysis and disturb metabolism of cancer cells [38, 39]. Herein, we synthesize CsLu$_2$F$_7$ nanoparticles with LA ligands (CsLu$_2$F$_7$-LA) for enhancing the effect of RT. As shown in Fig. 1a, after the synthesis of oleic acid (OA) modified CsLu$_2$F$_7$ (CsLu$_2$F$_7$-OA), LA can easily replace OA to obtain water-soluble CsLu$_2$F$_7$-LA because the strong acid can replace the weak one [40, 41]. As Cs and Lu are high-Z atoms, CsLu$_2$F$_7$-LA can deposit more X-rays in tumor area (Fig. 1b). In addition, CsLu$_2$F$_7$-LA will target and disturb the MCT on the cancer cell membrane to block the transportation of LA (Fig. 1b). Then the resultant accumulation of LA will limit the speed of glycolysis and inhibit the repair of DNA DSBs. As a result, the curative effect of RT will be enhanced obviously. We believe this research will bring new ideas and chances for the design of nanomaterials for enhanced RT.

**Materials and methods**

**Chemicals and reagents**

LuCl$_3$, cesium acetate (CsAc), lactic acid (LA), oleic acid (OA), 1-octadecene (ODE) and Rhodamine B (RhB) were purchased from Macklin. NH$_4$F, methanol, ethanol and cyclohexane were purchased from Sinopharm Chemical Reagent Co., Ltd. Phosphate buffered solution (PBS), dulbecco’s modified eagle medium (DMEM) and fetal bovine serum (FBS) were obtained from Adamas Life. Cell counting kit-8 (CCK-8), histone H2AX rabbit

![Fig. 1](image-url)  
**Fig. 1** Illustration of a synthetic procedure of CsLu$_2$F$_7$-LA and b the mechanism that CsLu$_2$F$_7$-LA enhance the effect of RT
polyclonal antibody, fluorescein isothiocyanate (FITC), FITC-labeled goat anti-rabbit IgG (H+L), DAPI staining kit, Ki67 staining kit, 2,7'-bis-(2-carboxyethyl)-5-(and-6)-carboxyfluorescein (BCECF) assay kit, 2,7-Dichloro-5-iodo-fluorescein diacetate (DCFH-DA) assay kit, ATP assay kit, hematoxylin and eosin (H&E) staining kit, TUNEL apoptosis assay kit, calcein/PI cell viability/cytotoxicity assay kit, Annexin V-FITC/PI apoptosis assay kit were bought from Beyotime.

Characterization
Transmission electron microscope (TEM) image was carried out by FEI Talos F200X. X-ray diffraction (XRD) was measured by Rigaku D/MAX-2250V. Dynamic light scattering was measured by Brookhaven omni. X-ray photoelectron spectroscopy (XPS) spectra was measured by Thermo Fisher Scientific ESCALAB 250XI. Confocal laser scanning microscopy was carried out on Leica TCS SP8 STED 3X. Fourier transform infrared spectroscopy (FTIR) was measured by Bruker Thermo Fisher Nicolet 6700. The concentration of Lu element was measured by inductively coupled plasma optical emission spectrometer (ICP-OES, Agilent 725). The fluorescence microplate system was TECAN SPARK. Flow Cytometer was BD FACSCalibur. Radiation therapy was carried out by clinical 220 keV X-ray (SARRP, Gulmay Medical Inc.).

Synthesis of CsLu$_2$F$_7$-OA and CsLu$_2$F$_7$-LA
2 mmol LuCl$_3$, 20 mL OA and 10 mL ODE were mixed in a flask with three necks and heated to 150 °C under the protection of N$_2$ for 1 h, and then cooled to room temperature. 7 mmol NH$_4$F and 1 mmol CsAc were poured into the flask and stirred for 1 h. Then this mixture was heated to 290 °C for 1.5 h and cooled to room temperature subsequently. After washed with ethanol and cyclohexane for three times, the obtained CsLu$_2$F$_7$-OA were dispersed in 10 ml cyclohexane. 10 ml as-prepared CsLu$_2$F$_7$-OA solution in cyclohexane and 10 ml LA solution in water (0.1 M) were mixed and stirred for 4 h. Then this mixture was washed with ethanol for three times, the obtained CsLu$_2$F$_7$-LA were dispersed in 10 ml water.

Detection of ·OH in solution
4 ml solution contained RhB (5 ppm) with CsLu$_2$F$_7$-LA (500 ppm) or water (control group) were placed in centrifuge tubes. These tubes were irradiated with 0 Gy, 5 Gy, 10 Gy, 15 Gy and 20 Gy of X-rays. Supernatants were collected after centrifugation. The ·OH yield was represented by the degradation rate of RhB (absorbance at 554 nm).

Cells and animals
143B cells (human osteosarcoma cells) and HUEVC (human umbilical vein endothelial cell) cells were purchased from Shanghai Institute of Biochemistry and Cell Biology, Chinese Academy of Sciences. Kunming mice and Balb/c nude mice were purchased from Shanghai SLAC Laboratory Animal Co. Ltd. All the experiments in vivo were approved by the animal ethics committee of Shanghai Jiao Tong University, and the ethics number was 20210918-02.

Cell viability
143B cells or HUVEC cells (10,000 cells/well) were seeded in the 96-well plates and cultured at 37 °C for 24 h. Next, the medium was replaced by the fresh DMEM medium containing LA and CsLu$_2$F$_7$-LA at different concentrations and cultured for another 24 h. 100 μl culture media containing 10 μl CCK-8 solution was added and co-incubated with cells for 2 h. The absorbance was measured using a microplate reader at 450 nm.

Cell apoptosis
143B cells (500,000 cells/well) were seeded in 6-well plates and cultured for 24 h. Then the cells were incubated with DMEM medium and CsLu$_2$F$_7$-LA (50 ppm) respectively for another 24 h. The cells were irradiated with X-ray (0 Gy or 4 Gy). After 12 h, flow cytometer with Annexin V-FITC/PI double staining was used to evaluate cell apoptosis.

Detection of DNA DSBs
143B cells (50,000 cells/well) were seeded in confocal dishes (diameter: 20 mm) and cultured for 24 h. Then the cells were incubated with DMEM medium and CsLu$_2$F$_7$-LA (50 ppm) respectively for another 24 h. The cells were irradiated with X-ray (0 Gy or 4 Gy). After 1 h, the cells were fixed by 4% paraformaldehyde for 15 min and washed three times with PBS. 0.2% Triton X-100 was added to penetrate cells for 10 min. Next, the 1% BSA dissolved in PBS was used to block the cells for another 1 h at room temperature. After incubation with γ-H2AX antibody overnight at 4 °C, the cells were treated with Anti-Rabbit IgG (H+L), F(ab')2 Fragment (Alexa Fluor®488 Conjugate) for 1 h and then stained with DAPI for 15 min. Lastly, the fluorescence of γ-H2AX was observed by a confocal fluorescence microscope.

Fluorescence imaging of live/dead cells and ROS
143B cells (50,000 cells/well) were seeded in confocal dishes (diameter: 20 mm) and cultured for 24 h. Then
the cells were incubated with DMEM medium and 
CsLu$_2$F$_7$-LA (50 ppm) respectively for another 24 h. 
The cells were irradiated with X-ray (4 Gy). After 24 h, 
the cells were incubated with calcein-AM and PI for 
0.5 h. For ROS detection, the cells were incubated with 
DCFH-DA for 0.5 h. After incubation, the fluorescence 
was observed by a confocal fluorescence microscope.

Fluorescence imaging of pH in vitro
143B cells (50,000 cells/well) were seeded in confocal 
dishes (diameter: 20 mm) and cultured for 24 h. Then 
the cells were incubated with DMEM medium and 
CsLu$_2$F$_7$-LA (50 ppm) respectively for another 24 h. After 
24 h, the cells were incubated with BCECF for 0.5 h. After 
incubation, the fluorescence was observed by a confocal 
fluorescence microscope.

Cell clone formation assay
143B cells were seeded in the 6-well plates at various 
densities of 500, 500, 1000, and 2000 cells/well for 24 h. 
Then the cells were incubated with DMEM medium and 
CsLu$_2$F$_7$-LA (50 ppm) respectively for another 24 h. After 
24 h, the cells were irradiated with 0 Gy, 2 Gy, 4 Gy, 6 Gy X-rays. 
After being cultured with fresh medium for 10 days, the 
cells were fixed with absolute methyl alcohol and stained 
with hematoxylin and eosin. The number of colonies was 
counted by Image-J.

In vivo biocompatibility assay
The standard H&E staining and blood parameter 
were conducted to monitor the biocompatibility of 
CsLu$_2$F$_7$-LA. The Kunming mice (7 weeks, female) were 
 injected with CsLu$_2$F$_7$-OA (0–80 mg/kg) through the tail 
vein. The main tissues (heart, liver, spleen, lung and kidney) of Kunming mice were dissected for H&E staining 
at 30 days post-injection. The blood of Kunming mice was harvested for blood routine test and biochemical 
analysis.

In vivo radiation therapy
To set up the xenograft tumor model, 143B cells (1 × 10$^6$ cells) were injected subcutaneously into Balb/c nude mice (7 weeks, female). When the tumor volume reached about 100 cm$^3$, the mice were divided four groups randomly: (i) Control, (ii) CsLu$_2$F$_7$-LA, (iii) Control + X-ray, 
(iv) CsLu$_2$F$_7$-LA + X-ray. PBS (10 μL) and CsLu$_2$F$_7$-LA (1 mg, 10 μL) were injected into tumors directly. After 24 h, the tumors of groups iii and iv were irradiated with 
X-rays (6 Gy). After 48 h, the H&E, TUNEL and Ki67 staining of the tumor tissues were performed by commercially available kits. The body weight and tumor volume of the mice were measured every 2 days.

Results and discussion
Synthesis and characterization of CsLu$_2$F$_7$-LA
As shown in Fig. 1a, CsLu$_2$F$_7$-LA are synthesized by the 
pyrolysis [42, 43]. We first use LuCl$_3$, OA and octadecene 
(ODE) to react at 150 °C to obtain the Lu precursor (lute-

cium oleate). Then this precursor is mixed with cesium 
acetate (CsAc) and ammonium fluoride (NH$_4$F), and react 
at 290 °C to obtain CsLu$_2$F$_7$-OA. To obtain CsLu$_2$F$_7$-LA, 
the CsLu$_2$F$_7$-OA cyclohexane solution is mixed with 
LA water solution for 24 h, during this process LA will 
gradually replace OA. As shown in Fig. 2a, transmis-
sion electron microscopy (TEM) image shows that 
CsLu$_2$F$_7$-OA is monodispersed with a size of ~10 nm, 
while the hydrodynamic radius of CsLu$_2$F$_7$-OA (Addi-
tional file 1: Fig. S1) measured by dynamic light scat-
tering (DLS) is 12.7 nm. The Fourier transform infrared 
(FTIR) spectra of CsLu$_2$F$_7$-OA (Additional file 1: Fig. S2) 
presents the strong absorption of methylene asymmetric 
carbon-hydrogen bonds (C-H) stretching and methane 
symmetric C-H stretching, which come from OA mole-
 

cules [44]. In contrast, CsLu$_2$F$_7$-LA has little absorption of 
C-H stretching, which proves the successful modifica-
tion of LA. After LA modification, CsLu$_2$F$_7$-LA present 
slight agglomeration (Fig. 2b), but still remain stable in 
deionized (DI) water, saline and dulbecco's modified 
eagle medium (DMEM) (Additional file 1: Fig. S3). The 
high angle annular dark field-scanning transmission electron microscopy (HAADF-STEM) image (Fig. 2c) and elemental mapping (Fig. 2d–f) show the existence of Cs atoms, Lu atoms, and F atoms in CsLu$_2$F$_7$-LA. In addition, the data of energy disperse spectroscopy (EDS) and X-ray photoelectron spectroscopy (XPS) also show that CsLu$_2$F$_7$-LA contain Cs, Lu and F elements (Fig. 2g, h and Additional file 1: Fig. S4). Finally, X-Ray diffraction (XRD) pattern shows that the crystal structures of CsLu$_2$F$_7$-OA and CsLu$_2$F$_7$-LA are in accordance with 
standrad sample (Fig. 2i), indicating that the LA modifi-
cation does not change the crystal structure of CsLu$_2$F$_7$. 
The yield of ·OH in solutions is detected by the degra-
dation of Rhodamine B (RhB). As shown in Additional 
file 1: Fig. S5, CsLu$_2$F$_7$-LA can induce more ·OH than 
control group (DI water), presenting that CsLu$_2$F$_7$-LA 
can deposit more X-rays.

CsLu$_2$F$_7$-LA impede the glycolysis in vitro
After the synthesis and characterization of CsLu$_2$F$_7$-LA, 
we clarify if they could disturb the glycolysis through 
blocking MCT. As shown in Fig. 3a, CsLu$_2$F$_7$-LA pre-
sent little cytotoxicity to human umbilical vein endothe-
 

tial cell (HUVEC) even at the concentration of 100 ppm 
(Lu atoms). While as shown in Fig. 3b, the same dos-
age of CsLu$_2$F$_7$-LA makes obvious damage to 143B
cells (human osteosarcoma cell). LA is a kind of molecule that exists in the human body, and present little cytotoxicity to 143B cells (Fig. 3c). In addition, it is worth noting that there are few free ions release from CsLu$_2$F$_7$-LA (Additional file 1: Fig. S6). Hence, we suppose that the cytotoxicity of CsLu$_2$F$_7$-LA to 143B cells can be attributed to the blocking of MCT. To verify this hypothesis, we detected the pH of 143B cells by 2',7'-bis-(2-carboxyethyl)-5-(and-6)-carboxyfluorescein (BCECF) staining. If CsLu$_2$F$_7$-LA block MCT, LA will accumulate in cells and the pH will decrease. As shown in Fig. 3d, e the fluorescence of BCECF of CsLu$_2$F$_7$-LA group is lower than that of control group, indicating CsLu$_2$F$_7$-LA can decrease the pH of 143B cells. Additionally, as shown in Fig. 3f, the decreased content of adenosine triphosphate (ATP) of CsLu$_2$F$_7$-LA group further prove that the accumulation of LA will impede the process of glycolysis. The cytophagy of CsLu$_2$F$_7$-LA is detected by confocal microscopy. CsLu$_2$F$_7$-LA are decorated with fluorescein isothiocyanate (FITC) through electrostatic adsorption. After co-culture for 4 h, the fluorescence of FITC is found in 143B cells, indicating that CsLu$_2$F$_7$-LA can enter into...
cells (Additional file 1: Fig. S7). All these data show that CsLu$_2$F$_7$-LA can impede glycolysis through blocking MCT.

CsLu$_2$F$_7$-LA enhance the effect of RT in vitro
Having proved that CsLu$_2$F$_7$-LA can slow down glycolysis, in this section, we explore the enhancement of CsLu$_2$F$_7$-LA to RT in vitro. Cell colony formation assay indicates that single CsLu$_2$F$_7$-LA can decrease the proliferation of cancer cells because of the deceleration of metabolism as mentioned above (Fig. 4a, b). Meanwhile, CsLu$_2$F$_7$-LA can also enhance the proliferative damage of RT with the increase of radiation dose (Fig. 4a, b). The staining of prodium iodide (PI) show that the combination of CsLu$_2$F$_7$-LA and X-ray can induce the most cell death (Fig. 4c, d). Apoptotic analysis measured by flow cytometry presents similar results (Figure S8). The enhancement of RT can be attributed to two reasons. For one thing, CsLu$_2$F$_7$-LA containing high-Z atoms, which can deposit more X-rays and increase the yield of ROS compared with other groups (Fig. 4e). For another, CsLu$_2$F$_7$-LA can decelerate glycolysis of cancer cells, leading to decreased repairment of DNA damage. Then it is not surprising that the combination of CsLu$_2$F$_7$-LA and X-ray can induce the most DNA DSBs (Fig. 4f and Additional file 1: Fig. S9), which will induce serious proliferative injury and cell death. Hence, these data prove that CsLu$_2$F$_7$-LA can enhance the effect of RT in vitro.

CsLu$_2$F$_7$-LA enhance the effect of RT in vivo
Encouraged by the experiments in vitro, we then verify the performance of CsLu$_2$F$_7$-LA in vivo. Firstly, the biological compatibility of CsLu$_2$F$_7$-LA is evaluated based on Kunming mice. As shown in Additional file 1: Fig. S10a, the body weights have no obvious differences among the groups injected with different dosage (0 mg/kg, 20 mg/kg, 40 mg/kg and 80 mg/kg) of CsLu$_2$F$_7$-LA. The blood biochemical indexes including alanine transaminase (ALT), aspartate transaminase (AST), alkaline phosphatase (ALP), urea and creatinine (CRE) of different dosage of CsLu$_2$F$_7$-LA also exhibit few differences (Additional file 1: Fig. S10b–f). Additionally, H&E staining of major organs (heart, liver, spleen, lung, and kidney) of each group present no pathological and anomalous regions (Additional file: Fig. S11). Hence, CsLu$_2$F$_7$-LA present favorable biological compatibility to normal tissues even at a dosage of 80 mg/kg.
Next, the curative effect of the combination of CsLu₂F₇-LA and X-ray is characterized. As shown in Fig. 5a, this experiment is based on 143B tumor-bearing mice. These mice are divided into four groups including Control group, CsLu₂F₇-LA group, Control + X-ray group and CsLu₂F₇-LA group. During the observation period the body weights of each group exhibit few differences (Fig. 5b). The data of curative effect (Fig. 5c) show that single CsLu₂F₇-LA and single X-ray can both limit the progression of tumor compared with Control group, and the combination of CsLu₂F₇-LA and X-ray present the best tumor suppression effect. Hematoxylin and eosin (H&E) staining, Ki67 staining, and terminal-deoxynucleoitidyl transferase mediated nick end labeling (TUNEL) staining of tumor sections also show that the combination of CsLu₂F₇-LA and X-ray can induce the most apoptosis and necrosis (Fig. 5d). All these data prove that CsLu₂F₇-LA can enhance the effect of RT in vivo.
Conclusions

In summary, we synthesize CsLu$_2$F$_7$-LA for increasing the curative effect of RT. The contained Lu and Cs atoms can deposit much more X-rays in the process of RT to generate higher amount of \cdot OH. Meanwhile, CsLu$_2$F$_7$-LA can target MCT and hinder the transportation of LA, which lead to decreased glycolysis and DNA damage repair. As a result, the cancer cells will suffer from serious DNA DSBs and the curative effect of RT will be enhanced. All the experiments in vitro and in vivo prove the favorable performance of CsLu$_2$F$_7$-LA as radiosensitizers by disturbing glycolysis. RT is suitable for weak and elderly cancer patients because of the short treatment process and little invasive damage. However, radiation resistance is a bottleneck problem that limits the effect of RT. Generally, the specific

![Fig. 5 Experiments in vivo. a Illustration of the experimental design. b The weights of tumor-bearing mice of each group (6 Gy, n = 5, mean ± SD). c Relative tumor volume of each group (6 Gy, n = 5, mean ± SD, triple asterisks indicate P < 0.001 according to Student’s two tailed t-test). d H&E staining, Ki67 staining and TUNEL staining of tumor sections. Scale bar: 100 μm.](image-url)
metabolism of cancer cells supports themselves with proliferation and treatment resistance [45, 46]. In this research, we disturb glycolysis through LA accumulation to increase the effect of RT. More metabolic targets such as glutamine metabolism, pentose phosphate pathway, and tricarboxylic acid cycle can be explored in the future.

Supplementary Information
The online version contains supplementary material available at https://doi.org/10.1186/s12951-022-01694-1.

Additional file 1: Figure S1. Hydrodynamic radius of CsLu2F7-OA measured by dynamic light scattering (DLS). Figure S2. FTIR spectra of CsLu2F7-OA and CsLu2F7-LA. Figure S3. Hydrodynamic size of CsLu2F7-LA dispersed in DI water, saline and DMEM at 1st day, 7th day and 14th day. Figure S4. Cs 3d, Lu 4d and F 1s X-ray photoelectron spectroscopy (XPS) spectrum. Figure S5. The yield of -OH in solutions upon irradiation of 0 Gy, 5 Gy, 10 Gy, 15 Gy and 20 Gy X-rays (n = 5, mean ± SD). Four asterisks indicate P < 0.0001 according to Student’s two-tailed t-test. Figure S6. Relative release of Lu atoms of CsLu2F7-LA in saline (n = 3, mean ± SD). Figure S7. Cytotoxicity of CsLu2F7-LA (50 ppm). CsLu2F7-LA were decorated with FITC. Scale bar: 100 μm. Figure S8. Apoptotic analysis measured by flow cytometry. Figure S9. Relative intensity of γ-H2AX in each group (n = 3, mean ± SD). Figure S10. Biological compatibility evaluation of CsLu2F7-LA. Figure S11. H&E staining of major organs (heart, liver, spleen, lung, kidney) 30 days post intravenous injection of different dosage of CsLu2F7-LA. Scale bar: 100 μm.

Author contributions
HL and HW carried out experiments and wrote the original manuscript. HL and HW contributed to sample preparation. YJX and DLN provided guidance and assistance on experiments. DLN performed the data curation. All authors read and approved the final manuscript.

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Availability of data and materials
All study data are included in this article.

Declarations

Ethics approval and consent to participate
The animal experiments were approved by the animal ethics committee of Shanghai Jiao Tong University.

Consent for publication
All authors read and approved the final manuscript for publication.

Competing interests
The authors declare that they have no competing interests.

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References
1. Barker HE, Paget JT, Khan AA, Harrington KJ. The tumour microenvironment: mechanisms of resistance and recurrence. Nat Rev Cancer. 2015;15:409–25.
2. Prise KM, O’Sullivan JM. Radiation-induced bystander signalling in cancer therapy. Nat Rev Cancer. 2009;9:351–60.
3. Herrera FG, Bourhis J, Coukos G. Radiotherapy combination opportunities leveraging immunity for the next oncology practice. CA Cancer J Clin. 2017;67:65–85.
4. Nolan E, Bridgeman VL, Ombroti L, Karoutas A, Rabas N, Sewnath CAN, Vasquez M, Rodrigues FS, Horwessel S, Faull P; et al. Radiation exposure elicits a neutrophil-driven response in healthy lung tissue that enhances metastatic colonization. Nat Cancer. 2022;3:173–87.
5. Song G, Cheng L, Chao Y, Yang K, Liu Z. Emerging nanotechnology and advanced materials for cancer radiation therapy. Adv Mater. 2017. https://doi.org/10.1002/adma.201700996.
6. Xie J, Gong L, Zhu S, Yong Y, Gu Z, Zhao Y. Emerging strategies of nanomaterial-mediated tumor radiosensitization. Adv Mater. 2019;31: e1802244.
7. Dou Y, Guo Y, Li X, Li X, Wang S, Wang L, Lv G, Zhang X, Wang H, Gong X, Chang J. Size-tuning ionization to optimize gold nanoparticles for simultaneous enhanced CT imaging and radiotherapy. ACS Nano. 2016;10:2536–48.
8. Her S, Jaffray DA, Allen C. Gold nanoparticles for applications in cancer radiotherapy: Mechanisms and recent advancements. Adv Drug Deliv Rev. 2017;109:84–101.
9. Gupta PB, Patsushenko I, Skibinski A, Blanpain C, Kuperswasser C. Photonic plasticity: driver of cancer initiation, progression, and therapy resistance. Cell Stem Cell. 2019;24:65–78.
10. Vriens K, Christen S, Panik S, Broekaert D, Yoshinaga K, Talebi A, Dehairs J, Escalona-Noguero C, Schmieder R, Cornfeld T; et al. Evidence for an alternative fatty acid desaturation pathway increasing cancer plasticity. Nature. 2019;566:403–6.
11. Krause M, Dubrovskova A, Linge A, Baumann M. Cancer stem cells: Radiosensitivity, prediction of radiotherapy outcome and specific targets for combined treatments. Adv Drug Deliv Rev. 2017;109:63–73.
12. Stapleton S, Jaffray D, Milosevic M. Radiation effects on the tumor microenvironment: Implications for nanomedicine delivery. Adv Drug Deliv Rev. 2017;109:119–38.
13. Milanovic M, Fan DNY, Belenki D, Dabritz JHM, Zhao Z, Yu Y, d’Oir JR, Dimitrova L, Lenze D, Monteiro Barbosa IA, et al. Senescence-associated reprogramming promotes cancer stemness. Nature. 2017;553:96–100.
14. Chen H, Zhang W, Zhu G, Xie J, Chen X. Rethinking cancer nanotheranostics. Nat Rev Mater. 2017. https://doi.org/10.1038/natrevmats.2017.24.
15. Wang J, Li Z, Wang Z, Yu Y, Li D, Li B, Ding J. Nanomaterials for combinational radio-immuno oncotherapy. Adv Funct Mater. 2020. https://doi.org/10.1002/adfm.201910676.
16. Chen J, Jiang Z, Zhang YS, Ding J, Chen X. Smart transformable nanoparticles for enhanced tumor theranostics. Appl Phys Rev. 2021. https://doi.org/10.1063/5.0061530.
17. Wang J, Xu W, Zhang N, Yang C, Xu H, Wang Z, Li B, Ding J, Chen X. X-ray-responsive polypeptide nanogel for concurrent chemoradiotherapy. J Control Release. 2021;332:1–9.
18. Yue S, Li Y, Qiao Z, Song W, Bi S. Rolling circle replication for biosensing, bioimaging, and biomedicine. Trends Biotechnol. 2021;39:1160–72.
19. Zheng P, Ding J. Calcium ion nanomodulators for mitochondria-targeted multimodal cancer therapy. Asian J Pharm Sci. 2022;17:1–3.
20. Zhang C, Wang H, Yang X, Fu Z, Ji X, Shi Y, Zhong J, Hu W, Ye Y, Wang Z, Ni D. Oral zero-valent-molybdenum nanodots for inflammatory bowel disease therapy. Sci Adv. 2022;8:eabbp9882.
21. Wang H, Guo J, Lin W, Fu Z, Ji X, Yu B, Lu M, Cui W, Deng L, Engle JW; et al. Open-shell nanosensitizers for glutathione responsive cancer sonodynamic therapy. Adv Mater. 2022;34: e2102083.
22. Cheng NN, Starkeff Z, Davidson RA, Sharma A, Lee C, Lien J, Guo T. Chemical enhancement by nanomaterials under X-ray irradiation. J Am Chem Soc. 2012;134:1950–3.
23. Yong Y, Zhang C, Gu Z, Du J, Guo Z, Dong X, Xie J, Zhang G, Liu X, Zhao Y. Polyoxometalate-based radiosensitization platform for treating hypoxic tumors by attenuating radioresistance and enhancing radiation response. ACS Nano. 2017;11:7164–76.

24. Song G, Chen Y, Liang C, Yi X, Liu J, Sun X, Shen Y, Yang K, Liu Z. Catalase-loaded TaOx nanoshells as bio-nanoreactors combining high-Z element and enzyme delivery for enhancing radiotherapy. Adv Mater. 2016;28:7143–8.

25. Song G, Liang C, Yi X, Zhao Q, Cheng L, Yang K, Liu Z. Perfluorocarbon-loaded hollow Bi2Se3 nanoparticles for timely supply of oxygen under near-infrared light to enhance the radiotherapy of cancer. Adv Mater. 2016;28:2716–23.

26. Wang H, Gao HB, Jiang XW, Zhao PR, Ni DL, Tang ZM, Liu YY, Zheng XP, Bu WB. Regulating water states by vacancies for cancer therapy. Nano Today. 2021;37:7.

27. Wang H, Lv B, Tang ZM, Zhang M, Ge WQ, Liu YY, He XH, Zhao KL, Zheng XP, He MY, Bu WB. Scintillator-based nanohybrids with sacrificial electron prodruk for enhanced x-ray-induced photodynamic therapy. Nano Lett. 2018;18:5768–74.

28. Huang W, He L, Ouyang J, Chen Q, Liu C, Tao W, Chen T. Triangle-shaped tellurium nanostars potentiate radiotherapy by boosting checkpoint blockade immunotherapy. Matter. 2020;3:725–53.

29. Gong T, Li Y, Lv B, Wang H, Li Y, Yang W, WU Y, Jiang X, Gao H, Zheng X, Bu W. Full-process radiosensitization based on nanoscale metal-organic frameworks. ACS Nano. 2020. https://doi.org/10.1021/acsnano.9b07898.

30. Rodrigues TB, Serrao EM, Kennedy BW, Hu DE, Kettunen MI, Brindle KM. Magnetic resonance imaging of tumor glycolysis using hyperpolarized 13C-labeled glucose. Nat Med. 2014;20:93–7.

31. Yaku K, Okabe K, Hikosaka K, Nakagawa T. NAD metabolism in cancer therapeutics. Front Oncol. 2018;8:622.

32. Zhao Y, Butler EB, Tan M. Targeting cellular metabolism to improve cancer therapeutics. Cell Death Dis. 2013;4: e332.

33. Birsoy K, Wang T, Possemato R, Yilmaz OH, Koch CE, Chen WW, Hutchins AW, Gultekin Y, Peterson TR, Carette JE, et al. MCT1-mediated transport of a toxic molecule is an effective strategy for targeting glycolytic tumors. Nat Genet. 2013;45:104–8.

34. Wen S, Zhu D, Huang P. Targeting cancer cell mitochondria as a therapeutic approach. Future Med Chem. 2013;5:53–67.

35. Liu X, Li Y, Wang K, Chen Y, Shi M, Zhang X, Pan W, Li N, Tang B. GSH-responsive nanoprodrug to inhibit glycolysis and alleviate immunosuppression for cancer therapy. Nano Lett. 2021;21:7862–9.

36. Wilson JE. Isozymes of mammalian hexokinase: structure, subcellular localization and metabolic function. J Exp Biol. 2003;206:2049–57.

37. Hirschkaeuser F, Sattler UG, Mueller-Klieser W. Lactate: a metabolic key element and enzyme delivery for enhancing radiotherapy response. ACS Nano. 2017;11:7164–76.

38. Song G, Chen Y, Liang C, Yi X, Liu J, Sun X, Shen Y, Yang K, Liu Z. Catalase-loaded TaOx nanoshells as bio-nanoreactors combining high-Z element and enzyme delivery for enhancing radiotherapy. Adv Mater. 2016;28:7143–8.

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