Quantifying structural connectivity in brain tumor patients

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Abstract. Brain tumors are characterised by infiltration along the white matter tracts, posing significant challenges to precise treatment. Mounting evidence shows that an infiltrative tumor can interfere with the brain network diffusely. Therefore, quantifying structural connectivity has potential to identify tumor invasion and stratify patients more accurately. The tract-based statistics (TBSS) is widely used to measure the white matter integrity. This voxel-wise method, however, cannot directly quantify the connectivity of brain regions. Tractography is a fiber tracking approach, which has been widely used to quantify brain connectivity. However, the performance of tractography on the brain with tumors is biased by the tumor mass effect. A robust method of quantifying the structural connectivity in brain tumor patients is still lacking. Here we propose a method which could provide robust estimation of tract strength for brain tumor patients. Specifically, we firstly construct an unbiased tract template in healthy subjects using tractography. The voxel projection procedure of TBSS is employed to quantify the tract connectivity in patients, based on the location of each tract fiber from the template. To further improve the standard TBSS, we propose an approach of iterative projection of tract voxels, under the guidance of tract orientation measured by voxel-wise eigenvectors. Compared to the conventional tractography methods, our approach is more sensitive in reflecting functional relevance. Further, the different extent of network disruption revealed by our approach correspond to the clinical prior knowledge of tumor histology. The proposed method could provide a robust estimation of the structural connectivity for brain tumor patients.

Keywords: brain networks · structural connectivity · brain tumor · tractography · diffusion MRI.

1 Introduction

1.1 Brain tumors and white matter tracts

A brain tumor refers to a mass lesion identified within the brain or related structures. Among them, gliomas and meningiomas are the most common primary
tumor types in adults. Impacts of tumors are characterized by diffuse infiltration and interference with the white matter tracts [24, 26], the neuronal fiber bundles forming a complex network connecting cortical regions. As a result, the tumor infiltration along white matter tracts may lead to structural disturbance of the brain[13].

Brain tumor patients frequently demonstrate neurological deficits that are not directly explained by the focal lesion [8]. Therefore, it is increasingly accepted that brain tumors may cause broader impacts to the global brain beyond the focal site through the white matter tracts [1]. Therefore, accurately measuring structural connectivity strength offers a promising imaging surrogate to detect the tumor-related brain alterations. Further, the pre-treatment mapping of the structural connectivity provides significance for the planning of both surgery and radiotherapy[18]

1.2 Connectivity strength measurement

Recent development of neuroimaging techniques have facilitated characterization of brain connectivity at the whole-brain level, based on diffusion MRI (dMRI). The derived fractional anisotropy (FA) map is commonly used to measure the tract strength. The tract-based spatial statistics (TBSS) is a method to estimate the strength of specific tracts using a FA skeleton derived by mapping the local maxima FA voxels to the template [19]. As a voxel-based method, however, TBSS fails to consider the spatial continuity of the fiber pathway, which has difficulties in multiple testing and tracking the fibers that tumor infiltrates along [4]. Further, as the projection procedure in TBSS is purely based on the FA values, the traditional TBSS does not consider the orientation of the tract fibers that are frequently affected in brain tumor patients.

Tractography is a widely-used fiber tracking method to measure the tract connectivity. This method has the advantage of detecting the fiber pathway with spatial consistency. Performing tractography on brain tumor patients, however, has the below challenges: 1) The tract pathways in vicinity to the tumor are often anatomically deviated, which may cause errors in fiber tracking. 2) Many brain tumors are remarkably heterogeneous [28, 11, 10, 27]. Particularly, the edema region surrounding the tumor may cause artefacts in fiber tracking, as the FA value is commonly affected in these regions [17].

1.3 Related work

The conventional tractography methods include Fiber Assignment by Continuous Tracking (FACT) and Unscented Kalman Filter (UKF) tractography.

**FACT tractography** FACT [14] is a deterministic method that tracks fiber streamlines from a seed region by following the primary eigenvector from one voxel to the next. FACT is highly sensitive to the changes of FA and tensor values
Quantifying structural connectivity in brain tumor patients in the white matter. As a result, the tracking frequently fails when encountering peritumoral edema, leading to overestimated disruption of the structural networks. In some other cases, it may produce spurious tract rings around the tumor, which may underestimate the connectivity reduction.[6]

**UKF tractography** UKF is shown to be able to track inside the peritumoral edema using two tensor models [12]. However, in order to achieve this, the model weakly controls the false positive fibers compared to healthy subjects [6]. The trade-off between false positive and false negative rates is challenging to be optimized among patients, which could particularly cause bias in the group analysis when individual tumors have heterogeneous extent of peritumoral edema.

1.4 Our contributions

We propose a method of estimating structural connectivity for network construction in brain tumor patients, without directly fiber tracking on patients (Fig. 1). Inspired by a method for traumatic brain injury [20], we firstly performed tractography on healthy controls and generated an unbiased tract template, with the location of each tract fiber derived. The TBSS approach was then employed to derive the skeletonized FA maps from patients, for estimating the connectivity strength of each specific tract in patients. To mitigate the bias in TBSS voxel projection caused by tumor mass effect, we further proposed an improved TBSS tailored to brain tumors, using an iterative projection of FA voxels guided by the tract orientation based on the voxel-wise eigenvector.

We compared the connectivity strength estimated by the proposed approach and the conventional tractography methods in multiple datasets of brain tumor patients. The results show that our approach is reflecting more functional relevance. Further, the different extent of network disruption revealed by our approach correspond to the clinical prior knowledge of tumor histology.

2 Methods

2.1 Datasets

Three datasets of glioma or meningioma patients were included, with both diffusion MRI (dMRI) and resting-state functional MRI (rs-fMRI) available: 1) 4 low-grade gliomas (LGGs), 5 high-grade gliomas (HGGs) and 2 meningiomas (dMRI: 60 directions, b = 1000 s/mm2; rs-fMRI: TR = 2.5 s) were obtained from [16]; 2) OpenNeuro database: 7 LGGs, 4 HGGs, and 14 meningiomas (dMRI: 101 directions, b = 0, 700, 1200, 2800 s/mm2; rs-fMRI: TR = 2.4 s) [2]. 3) an in-house dataset: 12 HGGs (dMRI: 12 directions for each b values, b = 0, 350, 650, 1000, 1300, 1600 s/mm2; rs-fMRI: TR = 2.43 s). In total, 11 LGGs, 21 HGGs and 16 meningiomas were included.
2.2 Template-based brain networks

The proposed method includes three main steps:

- Producing an unbiased tractography template (Fig. 1A),
- Generating individualized FA skeleton (Fig. 1B),
- Combining tractography template with FA skeleton to estimate the connectivity strength between each pair of brain regions in patients.

![Flowchart of network construction](image)

**Tractography template** An unbiased tract template was generated in four steps using ten age-matched elderly healthy controls obtained from the Alzheimer’s disease Neuroimaging Initiative (ADNI, http://adni.loni.usc.edu/).
1) A diffusion model was fitted at each voxel of dMRI using Bedpostx of FM-RIB software library (FSL, https://fsl.fmrib.ox.ac.uk/fsl/). Pairwise probabilistic tractography was performed between 90 regions of Automated Anatomical Labelling atlas (AAL) atlas [22] using Probtrackx2 to generate a path distribution map in healthy controls [5].

2) The path distribution map was nonlinearly transformed to standard MNI-152 space [7] using the Advanced Normalization Tools (ANTs)[3] and finally averaged, to produce a group distribution map for each tract. The maps were thresholded and binarized to preserve the top 5% strongest connections and generate a conservative tract atlas in the standard space.

Individual FA skeleton from iterative projection An FA skeleton of each patient was generated at the individualized native space using an improved TBSS approach.

1) FA maps of all patients were first non-linearly co-registered to the standard space using ANTs. In addition, the corresponding principal eigenvector V1 maps were also transformed to the standard space. Instead of using the patient group thinned FA skeleton, we used the standard FA skeleton of FSL as the target for projection to reduce bias introduced by tumor.

2) We further improved TBSS that only projects the voxels with local maximum value at the tract center on the FA skeleton. Specifically, we compared the principal eigenvector (V1) of the projected voxel to the the standard V1 and calculated the orientation difference using vector product. The voxels with the orientation difference over 90 degrees were discarded, where neighbor voxels were selected instead. The projection iteration continued until all voxels on the skeleton converged to minimum direction difference with the standard FA skeleton. Using this procedure, the continuity of the voxel directions on each tract could be improved. An individualized FA skeleton was generated in each patient.

Structural connectivity strength estimation The segments of the individualized FA skeleton within each tract of the template was extracted and averaged, representing the connectivity strengths of the major tracts.

2.3 Baseline methods
FACT was performed using diffusion toolkits [25], while UKF was performed using the UKFTratography packages in 3D Slicer(https://www.slicer.org/) via the SlicerDMRI project (http://dmri.slicer.org) [30, 15]. For both methods, the mean FA value of the tracts connecting two ROIs of AAL atlas was calculated using MRTrix3 by sampling and averaging the FA values along the streamlines generated by the tractography [21].

2.4 Functional brain networks
We constructed functional networks from rs-fMRI using GRETNA[23]. Firstly, the rs-fMRI signals were regressed, bandpass-filtered, smoothed with a kernel
with a full width at half maximum of 6mm and co-registered to the standard space. Secondly, the brain regions of each patient were parcellated using the AAL atlas. Finally, pairwise Pearson correlation was performed between the mean rs-fMRI signals in 90 brain regions.

2.5 Functional relevance of the structural networks

Whole-brain structural and functional connectivity coupling To measure the individualized functional relevance of a structural network, we calculated the whole brain structural connectivity-functional connectivity (SC-FC) coupling. Spearman rank correlation was performed between the non-zero elements of the structural connections with their corresponding functional connections to produce correlation coefficient for each patient. To compare the group difference, the correlation coefficients were transformed using Fisher Z-Transformation.

Group-wise structural-functional connection correlation The strength of functional connections varies due to the distinct extent of disruptions in corresponding structural connections. By testing the correlation of each functional and structural connection, the functional connections sensitive to structural damage can be identified. To weakly control the family-wise error in multiple comparisons, we used the network-based statistics (NBS)[29], providing higher sensitivity in controlling false discovery rate.

2.6 Clinical validation

The clinical prior knowledge establishes that meningiomas normally cause less disturbance to the brain than gliomas. A robust network construction method should be sensitive to the difference between meningioma and glioma. We used the global efficiency, calculated according to graph theory, to characterize the brain networks, which were compared in meningioma and glioma patients [9].

3 Results

3.1 Iterative TBSS projection

The proposed approach showed smaller orientation differences between patient FA skeleton and standard FA, compared to the baseline methods (Table 1). One example is illustrated on Fig. 2. Tracts that are displaced by the tumor have voxels from the wrong directions projected onto the FA skeleton. In comparison, our approach could ensure the maximum orientation continuity of the tracts.

3.2 Whole brain structural and functional connectivity coupling

The proposed method achieved higher SC-FC coupling over the baseline methods (Table 2), suggesting the robustness of the brain network constructed using the proposed method.
Table 1. Mean orientation differences between patient FA skeleton and standard FA

|                     | Traditional TBSS projection (radians) | Iterative TBSS projection (radians) | P-value   |
|---------------------|---------------------------------------|------------------------------------|-----------|
|                     | 0.424 ± 0.057                         | 0.388 ± 0.035                      | 3.8e-4    |

Table 2. SC-FC Coupling coefficient (z-transformed)

| Methods   | Mean ± SD | P-value (vs FACT) | P-value (vs UKF) |
|-----------|-----------|-------------------|------------------|
| Proposed  | 0.25 ± 0.07 | 3.3e-26           | 3.5e-8           |
| UKF       | 0.16 ± 0.08 | 3.8e-10           | -                |
| FACT      | 0.07 ± 0.05 | -                 | -                |

Fig. 2. Example of voxel projection in coronal (left), axial (middle) and sagittal (right) views. A. T1 contrast MRI indicating tumor location. B. Traditional TBSS voxel projection: the tracts surrounding the tumor display different direction (green) from the contralesional tract (blue). C. The proposed method improves the direction continuity of the tract.

3.3 Group-wise structural-functional connection correlation

Only the proposed method identified significantly correlated functional and structural sub-networks across the patient group, suggesting its high sensitivity to functional related structural disruptions. (Fig.3)

3.4 Global efficiency of different tumor types

The meningioma group in general has significantly higher global efficiency than the glioma group (P = 2.9e-4), while the baseline methods did not capture
Fig. 3. A. Sub-network is identified by the proposed method, with clusters of significantly correlated structural and functional connections ($P = 0.0014$). B. Fewer correlated structural and functional connections are identified by the UKF ($P > 0.05$). Family wise errors of both methods are corrected by NBS with 5000 permutations.

Fig. 4. Global efficiency of the structural networks constructed using the proposed method, FACT, and UKF. Compared to glioma, meningioma patients display significantly higher global efficiency in the network constructed using the proposed approach. ∗: $P < 0.05$
significant difference in Fig. 4. Further, in a subgroup of meningioma and high-grade glioma with comparable size, meningioma patients still have significant higher global efficiency comparing to high-grade glioma group ($P = 9.3\text{e-5}$), while baseline methods did not show significant difference.

4 Conclusion

This study proposes an approach to construct structural network and estimate the connectivity, which employs an improved TBSS approach and the tractography template from healthy controls. This method is shown to be robust compared to the conventional tractography, with higher functional and clinical relevance. The proposed method shows promise to aid treatment planning and patient risk assessment.

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