Evidence for a protein tether involved in somatic touch

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The gating of ion channels by mechanical force underlies the sense of touch and pain. The mode of gating of mechanosensitive ion channels in vertebrate touch receptors is unknown. Here we show that the presence of a protein link is necessary for the gating of mechanosensitive currents in all low-threshold mechanoreceptors and some nociceptors of the dorsal root ganglia (DRG). Using TEM, we demonstrate that a protein filament with of length ~100 nm is synthesized by sensory neurons and may link mechanosensitive ion channels in sensory neurons to the extracellular matrix. Brief treatment of sensory neurons with non-specific and site-specific endopeptidases destroys the protein tether and abolishes mechanosensitive currents in sensory neurons without affecting electrical excitability. Protease-sensitive tethers are also required for touch-receptor function in vivo. Thus, unlike the majority of nociceptors, cutaneous mechanoreceptors require a distinct protein tether to transduce mechanical stimuli.

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Introduction

Different classes of ion channel proteins can be opened by ligands, voltage or temperature (Fain, 2003). A fourth class of ion channels can be opened by mechanical force and such mechanosensitive channels are thought to underlie mechano-electric transduction in sensory cells (Gillespie and Walker, 2001; Hu et al, 2006; Wetzel et al, 2007). Essentially two models of gating have been proposed for sensory mechanosensitive channels. In the first model, force changes within the lipid bilayer act directly on the channel protein to facilitate opening and this model has been largely proven for bacterial mechanosensitive channels like MscL and MscS (mechanosensitive channels of large or small unitary conductance) (Sukharev et al, 1993, 1994; Kung, 2005). Members of another class of mammalian potassium channels belonging to the two pore potassium channel family have also been shown to be gated by force changes in the lipid bilayer (Honore, 2007). In the second model, protein tethers are proposed to transfer force from the surrounding matrix to the ion channel to promote opening (Chalfie, 2009). The tether model is well-supported for hair cells of the inner ear where a protein filament called the tip link, thought to consist of cadherin-23 and protocadherin-15 (Siemens et al, 2004; Sollner et al, 2004; Ahmed et al, 2006; Kazmierczak et al, 2007), may link ion channels at the tips of the stereocilia bundle where mechanotransduction takes place (Assad et al, 1991; Lumpkin and Hudspeth, 1995; Beurg et al, 2009). The tip link is necessary for mechanotransduction as shown by tip-link ablation experiments (Assad et al, 1991). Nevertheless, it is still unclear whether the tip link attaches directly to mechanosensitive ion channels or whether the tether molecule alters the force profile in the lipid bilayer around the channel (Kung, 2005). New evidence that rat hair cell mechanotransduction channels are predominantly located on the second and third row of stereocilia has ignited a debate as to whether tip links are directly connected to the transduction channels (Beurg et al, 2009; Spinelli and Gillespie, 2009).

The vast majority of mechanosensitive receptors in the body are sensory neurons of the dorsal root ganglia (DRG). Unlike hair cells, the mechanosensitive endings of sensory neurons are at a considerable distance from the cell body in vivo, in man this can be a distance of 1 m or more. Although the available evidence strongly suggests that mechanosensitive channels mediate the primary transduction event in mammalian sensory neurons, direct recording of transduction channel activity in situ has not been achieved (Hu et al, 2006). However, there are several examples of invertebrate mechanoreceptors in which the transduction current can be measured and these currents are necessary for mechanoreceptor function (Swerup et al, 1983; Hoger et al, 1997; O’Hagan et al, 2005). An alternative to recording transduction currents in situ is to measure the activity of mechanosensitive currents in acutely isolated sensory neurons (McCarter et al, 1999; Drew et al, 2002; Hu and Lewin, 2006; McCarter and Levine, 2006; Lechner et al, 2009). There is good evidence indicating that mechanosensitive currents...
measured in acutely isolated sensory neurons are physiologically relevant for mechanoreceptor function in vivo. For example, deletion of the gene encoding stomatin-like protein-3 (STOML3 or SLP3) in mice leads to loss of mechanoreceptor function and abolishes mechanosensitive currents measured in isolated neurons (Wetzel et al., 2007). There are three distinct types of mechanosensitive currents in sensory neurons, which have been named according to their inactivation/adaptation kinetics, one is rapidly adapting (RA), one slow-adapting (SA) and one intermittently adapting (IA) (Hu and Lewin, 2006). The RA-mechanosensitive current has a very different ion permeability and pharmacology from that of the IA- and SA-mechanosensitive currents (Hu and Lewin, 2006; Drew et al., 2007). Indeed, all three types of mechanosensitive current appear at different time points during embryonic development and their appearance is regulated by different mechanisms (Lechner et al., 2009). The amplitude of the RA-mechanosensitive current in nociceptors has also been shown to be modulated by activation of G-protein-coupled receptors as well as through nerve growth factor signalling (Di Castro et al., 2006; Lechner and Lewin, 2009; Lechner et al., 2009).

In the present study we asked whether a tether model applies to mechanotransduction in mammalian DRG neurons that mediate our sense of touch. We subjected cultured sensory neurons to a range of different treatments that disrupt matrix-cell interactions and then measured the consequences for mechanosensitive currents. We found that treatment with specific proteases alone was capable of specifically abolishing the activity of the RA-mechanosensitive current. Using transmission electron microscopy (TEM) we showed that such treatments also specifically ablate a large protein tether (~100 nm) that links sensory neuron membranes to a laminin matrix. The loss and reappearance of mechanosensitive currents was always linked to the presence of this tether. Experiments performed using intact skin-nerve preparation demonstrated that proteolytic cleavage specifically ablates the mechanosensitivity of touch receptors and thus reproduces the effects observed in vitro. Our study shows that extracellular links are necessary for the mechanosensitivity of somatic sensory afferents.

**Results**

Only the terminal endings of sensory neurons in the skin are mechanosensitive in vivo, and we thus sought to establish an in vitro model of the cellular milieu found at the receptor ending. To this end, adult mouse sensory neurons were cultured on a monolayer of mouse 3T3 fibroblasts. Sensory neurons grow neurites on fibroblasts and mechanical stimulation of these neurites (750 nm amplitude displacement) evoked fast mechanosensitive currents, as measured using whole-cell recording from the nearby cell body (Figure 1A and B). Using such stimuli it was observed that >98% of isolated sensory neurons (n = 45) possessed one of three mechanically activated currents, RA (inactivation in < 5 ms), IA (inactivation in < 50 ms) and SA (no adaptation during a 230 ms stimulus) (for examples see Figure 2A). Indeed the amplitude and kinetic parameters of neuritic mechanosensitive currents were identical to those observed on a standard laminin substrate obtained from matrix derived from Engelbreth–Holm–Swarm (EHS) cells (Invitrogen) (Figure 1A and B) (Hu and Lewin, 2006). We hypothesized that if mechanosensitive ion channels are gated by a tether linking them to the fibroblasts or matrix surrounding the fibroblast, then mechanical displacement of the fibroblast adjacent to the neurite may evoke fast mechanosensitive currents in sensory neurons. We found that in almost all cases (16/17 neurons) short-latency, fast-activating mechanosensitive currents were indeed evoked in sensory neurons when adjacent fibroblasts were mechanically stimulated (Figure 1A and B, and Supplementary Video S1). Compared with direct stimulation of neurites, the latency and activation time constant of the mechanosensitive current was virtually identical after mechanical stimulation of the adjacent fibroblast (Figure 1B). Most of the neurons recorded with a fast-evoked mechanosensitive current in response to mechanical stimulation
of adjacent fibroblasts, had an RA-mechanosensitive current (10/16). However, we also recorded fast SA- and IA-mechanosensitive currents in response to fibroblast stimulation (4 SA, 2 IA). The fact that the latency and activation of the mechanosensitive current evoked by stimulation of the neurite or adjacent fibroblast was not different, suggests that a physical link might transfer force from the stimulated fibroblast to mechanosensitive ion channels in the sensory neuron.

We next prepared sensory neuron/fibroblast co-cultures for TEM using fixation and staining procedures optimized to visualize extracellular proteins (see section Materials and methods). At the ultrastructure level we were able to distinguish fibroblast cells from neuronal profiles by the presence of neurofilament and the high density of mitochondria in sensory cells. Careful examination of many TEM sections revealed occasional long, tether-like links between fibroblasts and sensory neurites (Figure 1C). Such tethers are candidate entities for transferring force from matrix produced by fibroblasts and mechanosensitive channels. Electron microscopy was, however, challenging in this mixed culture system and clearly identifiable neurite/fibroblast interfaces were rare. Our data showed that the physiological properties of the mechanosensitive currents are indistinguishable when measured from neurons in neuron/fibroblast co-cultures or on laminin substrates (Figure 1B). We thus reasoned that if protein tethers are relevant for the function of mechanosensitive currents, they should also be present in sensory neurons cultured on laminin substrates (see below). We measured mechanosensitive currents in sensory neurons cultured on laminin (EHS-derived) as well as on laminin-111, a highly purified, trimeric laminin-a1b1g1–nidogen complex (Paulsson et al., 1987). We found that the incidence of mechanosensitive currents, their kinetic properties and amplitudes were not different between neurons plated on laminin or laminin-111 (Figure 2A). We also measured the mechanosensitive current in neurons plated only on a poly-L-lysine substrate (PLL); such neurons attach poorly and only some neurons actually extend neurites (data not shown). We found that 43% (8/17 neurons tested) lacked mechanosensitive currents when plated on the PLL substrate, a proportion

Figure 2 Subtilisin and blisterase selectively abolish RA-mechanosensitive currents. (A) Examples of RA-, IA- and SA-mechanosensitive currents evoked by stimulating sensory neuron neurites. Stacked histograms of the proportion of the three types of mechanosensitive current observed in controls (laminin and laminin-111) as compared with those in cultures treated with agents that disrupt extracellular matrix–cell interactions. The number of recorded neurons is indicated at the top of each stacked histogram. The empty bars indicate neurons in which no mechanosensitive current could be measured. (B) Local perfusion of single neuron with subtilisin leads to complete loss of the RA-mechanosensitive current (left); the current injection is, however, still effective at initiating APs. (C) The resting membrane potential (RMP), and the threshold current for AP initiation, was measured 0–3 h after subtilisin (red bars) or blisterase treatment (grey bars); the data were analysed separately for large (>25 µm diameter) and small neurons (<25 µm diameter); no differences were noted as compared with controls (black bars). Error bars represent ± s.e.m.
substantially higher than that found on laminin, which was 7% (3/42 neurons tested), and this was significant, with $P<0.05$ on $\chi^2$-test. We also noted that in cases where a mechanosensitive current was measured, there was always a nearby fibroblast that may have secreted a laminin-containing substrate.

We next conducted a series of experiments to examine the effects of manipulating extracellular matrix integrity or matrix–cell interaction on the mechanosensitive current measured in neurons plated on laminin. Hair cell tip-link proteins are rapidly disrupted by Ca$^{2+}$ chelation, consistent with the calcium dependence of cadherin interactions (Assad et al., 1991; Zhao et al., 1996; Siemens et al., 2004; Sollner et al., 2004; Kazmierczak et al., 2007). However, depleting extracellular Ca$^{2+}$ ions with the calcium chelator 1,2-bis(o-aminophenoxy)ehtane-N,N,N,N-tetraacetic acid (BAPTA) for 30 min had no effect on the incidence of the three types mechanosensitive currents. Indeed we, like others, noted that the amplitude of mechanosensitive current increased after exposing neurons to calcium-free solutions (Supplementary Table S1), which is consistent with partial calcium block of the mechanosensitive channel (Drew et al., 2002; Lechner et al., 2009). It has been suggested that integrin receptors might play a role in the transduction of mechanical stimuli in sensory neurons (Khalsa et al., 2004); we therefore blocked integrin signalling with the CD29 antibody (Mendrick and Kelly, 1993; Tomaselli et al., 1993). However, such treatments had no effect on the incidence or kinetic properties of mechanosensitive currents. A large number of membrane proteins are known to be glycosyl phosphatidylinositol (GPI)-anchored (Kinoshita et al., 2008), and some of them, like the channel-activating protease, (CAP1) can regulate mechanotransduction-related channels (Vallet et al., 1997). We thus used the enzyme phosphatidylinositol-specific phospholipase-C (PIPLCL) to cleave GPI anchors from the membrane. A large number of membrane proteins are thought to be GPI-anchored (Kinoshita et al., 2008), but this treatment again did not affect the kinetic properties, integrity and proportion of cells with a mechanosensitive current in sensory neurons (Figure 2A and Supplementary Table S1).

To address the possibility that an extracellular protein may be required for mechanosensitive current function, neurons in culture were subjected to limited proteolysis using soluble non-specific endopeptidase subtilisin during the recordings. We first locally treated sensory neurons with the enzyme phosphatidylinositol-specific phospholipase-C (PIPLCL) to cleave GPI anchors from the membrane. A large number of membrane proteins are thought to be GPI-anchored (Kinoshita et al., 2008), but this treatment again did not affect the kinetic properties, integrity and proportion of cells with a mechanosensitive current in sensory neurons (Figure 2A and Supplementary Table S1).

The blisterase enzyme is derived from the pathogenic nematode O. volvulus, but has been shown to have essentially the same substrate specificity as the human furin enzyme (Nakayama, 1997; Poole et al., 2003). We therefore conducted a series of experiments where we treated sensory neuron cultures with a soluble truncated human furin enzyme (Bravo et al., 1994). We found that at similar concentrations to blisterase (100 U ml$^{-1}$, 25–45 min, 37°C), pre-incubation of cultures with furin led to significant and substantial loss of RA-mechanosensitive current in mechanoreceptors. Thus, 8/13 neurons with APs characteristic of mechanoreceptors completely lacked the mechanosensitive current after prior furin treatment, and this was significantly different from that observed in control cultures with furin.
in the control cultures (0/19 mechanoreceptors lack the mechanosensitive current, \( \chi^2 \)-test \( P<0.001 \)). We also used 10 times lower concentrations of the furin enzyme (10 U ml\(^{-1} \), up to 900 min, 37 °C), but found no significant effect on the presence of mechanosensitive currents (data not shown). It appears that the two site-specific proteases, blisterase and furin, have very similar effects. We used the blisterase enzyme in further experiments as this enzyme appeared to be slightly more efficient than furin.

Following ablation of the hair cell tip link, mechanotransduction is lost, but transduction currents return 24 h later, correlated with the appearance of new tip-link proteins to the bundle (Zhao et al, 1996). We measured mechanosensitive currents in populations of cells 17–30 h after subtilisin removal. At these time points the incidence of the RA-mechanosensitive current had returned to control values and the latency and kinetics of these currents were identical to those in the controls (Supplementary Table S2). Thus, since sensory neurons are the major cell type in the culture, it appears that the cleaved extracellular peptide can be re-inserted into the membrane after cleavage to reinstate mechanosensitive current function. Recordings made at intermediate time points after subtilisin treatment did not show full recovery of the mechanosensitive current (data not shown).

We next asked whether anatomically identifiable protein tethers, that are subtilisin/blisterase-sensitive, could be responsible for RA-mechanosensitive current gating. We performed a quantitative TEM analysis comparing electron-dense attachments between the sensory neurite membrane and the laminin substrate under five conditions: control, subtilisin-treated acute (3 min) or subtilisin-treated 30-h recovery, blisterase-treated acute (25 min) and PIPLC treated (120 min). We could visualize an electron-dense laminin matrix 17 ± 1 nm in depth on the surface of the culture dishes, with a variety of tight and loose electron-dense connections between the neurite membrane and the matrix (Figure 4B).

The longest connecting objects were similar in length (~100 nm) and shape to those observed in TEM of sensory neuron/fibroblast co-cultures (Figures 1C and 4B). The strongest protein tethers were very rarely observed in subtilisin- or

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**Figure 3** Protease treatment does not affect other ion channels. (A) Example traces of whole-cell currents evoked by a series of step depolarization steps from a −120-mV pre-pulse potential in 10-mV steps, to +50 mV. The black traces are from the neurons before subtilisin treatment and the red traces were obtained post-subtilisin; no major change was seen in the kinetics or amplitudes of inward and outward currents. (B) Mean whole-cell inward and outward currents measured at different test potentials for all control cells (black) and cells treated acutely with subtilisin (red) or blisterase (blue). At each test potential, the peak inward current peak outward current at steady state was measured. Neurons treated with subtilisin showed small, but significant, leftward shift in the voltage for peak activation of the inward current (asterisks indicate data points significantly different from the control; two-way ANOVA, Bonferroni post hoc test \( P>0.01 \)). No change was observed in blisterase-treated cells as compared with that in the controls. (C, D) Proton-gated currents are not altered after subtilisin and blisterase treatment. The peak sustained (example trace in panel C) and transient (example trace in panel D) were not altered after subtilisin treatment. The amplitudes of proton-gated currents measured with stimuli of pH 6.0, 5.0 and 4.0 were not significantly different between control (black), subtilisin-treated (red) and blisterase-treated (blue) cells. The numbers of cells measured in each group is indicated in parentheses above each column.
Figure 4 TEM reveals a protein filament necessary for mechanotransduction. (A) Light photomicrograph of a cultured sensory neuron with a neuritic tree. The TEM photomicrographs were generated from ultrathin sections from blocks of tissue, with dimensions in the range illustrated by the white rectangle at the end of red dotted lines. (B) Sample electron micrographs of the neurite–matrix interface under a series of conditions, including, in each case, a quantification of the length of each measured attachment plotted in random two-dimensional space to illustrate the range of attachment lengths observed (right). Objects larger and smaller than 75 nm are demarcated by the red line. For each experimental condition, two sample photomicrographs are shown: one field illustrating tight attachment of the plasma membrane to the substrate and one a looser attachment area, with or without long protein tethers. For each experimental condition, a colour code is applied as follows: from the top, control (black), subtilisin acute (red), subtilisin recovery (purple), blisterase treatment acute (green), PIPLC treatment acute (cyan) and SCG neurons on laminin (orange).
blisters-treated cultures, but the incidence was essentially the same in the control and subtilisin-treated 30-h recovery group (Figure 4B). We quantified these data by randomly photographing microscopic fields in between 58 and 99 ultrathin sections (thickness 50 nm) from two to four cultures in each group and measured the number and length of the electron-dense objects that linked the neurite membrane to the laminin substrate (see Supplementary Table S3). The measured area of membrane contact was between 4.66 and 9.42 μm² in each group; the length of each object was then randomly plotted in two-dimensional space (Figure 4B). It is obvious from this representation of the raw data, that links with length between 5 and 75 nm were largely unaffected by subtilisin/blisterase treatment. However, electron-dense objects >75 nm in length, presumably corresponding to protein filaments, were selectively abolished after subtilisin/blisterase treatment (Figure 4B), but reappeared in cultures allowed to recover for 30 h after subtilisin treatment (Figure 4B). The final PIPLC-treated group served as control for enzymatic digestion of the sensory neuron culture per se. Electron-microscopic analysis of such cultures revealed no change in the incidence of filaments >75 nm (Figure 4B); nevertheless there was a significant shift in the mean size of electron-dense objects <75 nm in length (Supplementary Table S3), which probably reflects the shedding of a diverse group of GPl-anchored membrane proteins. It is conceivable that mechanosensitive currents are lost after protease treatment because of neurite detachment from the culture dish. If this were so then the long tether may be lost not because of proteolysis, but rather because of membrane detachment. To control for this possibility, all the sections were analysed to measure the average interface distance between the neurite membrane and the laminin substrate. As can be seen in the example electronmicrographs in Figure 4B, the physical distance can vary considerably along the contact zones. We found no significant difference between the mean neurite/laminin interface distance of 77 ± 8 nm in the control cultures as compared with 99 ± 8 nm in subtilisin-treated cultures and 80 ± 6 nm in blisterase-treated cultures (P > 0.05, Student’s t-test). We and others have previously shown that RA-mechanosensitive currents can readily be evoked by stimulation of the cell soma (McCarter et al, 1999; Drew et al, 2002, 2004; Hu and Lewin, 2006; McCarter and Levine, 2006; Lechner and Lewin, 2009; Lechner et al, 2009), and this raises the question whether the tether protein identified here is present at the soma–laminin interface. However, we were in fact able to observe tether-like filaments at soma–laminin interfaces (see example in Supplementary Figure S2); thus, stimulation of the soma may also gate mechanosensitive currents via an extracellular protein tether.

The subtilisin/blisterase-sensitive protein filament identified in our TEM experiments may be necessary for the gating of the RA-mechanosensitive current. To further test whether the long protein tether is specifically associated with the RA-mechanosensitive current, we recorded from superior cervical ganglion neurons (SCG) cultured on laminin. Sympathetic neurons are autonomic efferent neurons that have been reported not to possess mechanosensitive currents (Drew et al, 2002). We could confirm that no RA-mechanosensitive currents are observed in any of the recorded SCG neurons (Figure 5A). A detailed TEM study showed that no extracellular protein filaments are found that are greater than 75 nm in length, in SCG neuronal cultures (Figure 4B). Thus, among peripheral neurons it is only sensory neurons with a mechanosensory function that appear to synthesize a long tether-like protein when cultured on a laminin substrate.

In summary, our data suggest a model where a subtilisin/blisterase-sensitive protein filament links mechanosensitive ion channels in the membranes of sensory neurons to a laminin-containing matrix. Measurement of electron-dense objects longer than 75 nm in sensory neuron cultures showed that these long protein filaments average 100 ± 3 nm in length and occur with an average density of 4.9 ± 1.3 filaments per μm² of membrane (Supplementary Table S3). The tether-like protein is synthesized by sensory neurons as demonstrated by its recovery after 17–30 h in cultures briefly treated with the subtilisin protease. TEM analysis shows that one end of the filament attaches to the laminin-containing matrix. The fact that the tether-like protein is present when the RA-mechanosensitive currents are functioning and is absent or much reduced in situations where the RA-mechanosensitive currents are unresponsive to touch (Figure 5A) would suggest that this tether functions in a similar manner.

Figure 5 Superior sympathetic neurons lack an RA-mechanosensitive current (A). A stacked histogram of the proportion of three types of mechanically activated currents designated RA (dark blue), SA (medium blue) or IA (light blue) observed in DRG neurons and SCG neurons. (B) Example of a SA-mechanosensitive current recorded in an SCG neuron.
current is also reduced, suggests that this protein is likely necessary for the gating of the RA-mechanosensitive current. Further strong evidence for a mechanosensory role for this protein is the fact that peripheral non-mechanosensory neurons, lacking an RA-mechanosensitive current, do not synthesize tether-like proteins >75 nm in culture (Figures 4 and 5).

The question arises whether subtilisin-sensitive protein filaments may be required for mechanoreceptor function in situ. We applied the subtilisin enzyme (50 µg µl⁻¹) to the receptive fields of single identified mechanoreceptors and nociceptors recorded using the in vitro skin-nerve preparation (Martinez-Salgado et al., 2007; Milenkovic et al., 2008). When using a standard supra-threshold mechanical stimulus (ramp and hold displacement between 48 and 96 µm, for 2 s every 60 s), the mechanoreceptor response in most neurons remained very stable for periods greater than 20 min up to 90 min (data not shown). However, between 3 and 8 min after application of subtilisin enzyme, 50% of all the low-threshold mechanoreceptors displayed no mechanosensitivity (Figure 6A). The median survival time for the loss of mechanosensitivity was shortest for RA and SA mechanoreceptors (SAMs and RAMs) at 3–4 min and longest for D-hair mechanoreceptors at 8 min (Figure 6B). By the end of the observation period, virtually all mechanoreceptors were mechanically insensitive. For each treated afferent included in this analysis, electrical stimulation with a metal electrode placed in the receptive field at the end of the experiment evoked the same spike as was observed before commencement of treatment. Thus mechanosensitivity, but not electrical excitability, was abolished by subtilisin treatment (Figure 6A). In contrast, when mechanosensitive nociceptors with Aδ-axons were subjected to the same protocol, no effect on mechanosensitivity was observed (Figure 6B). In addition to being observed in mechanoreceptors, the RA-mechanosensitive current is also observed in a proportion of small sensory neurons in vitro that probably give rise to C-fibre nociceptors (Hu and Lewin, 2006; Lechner and Lewin, 2009). Consistent with this finding, we found that the mechanosensitivity of some, but not all, C-fibre nociceptors was attenuated by subtilisin treatment; however, this effect did not reach statistical significance (Figure 6B). The data from all the skin-nerve preparation experiments were also analysed in terms of the mean spike response per stimulus before and after application of subtilisin and the results were found to be similar (Supplementary Figure S3).

SA-mechanosensitive currents are found exclusively in nociceptors (Hu and Lewin, 2006) and the incidence of these currents and their kinetic properties were largely unaffected by protease treatment (Figure 2). However, SA-mechanosensitive currents were not completely insensitive to protease treatment as the mean latency for current activation more than doubled in neurons pretreated with subtilisin, blisterase and furin (even at the lower dose of 10 U ml⁻¹) (Figure 7A and B). The latency measured for the SA-mechanosensitive current had recovered to control values after a 17- to 30-h recovery period. Thus, subtilisin/blisterase-sensitive polypeptides are necessary for the normal kinetics of the SA current, but are not required for current activation. After treatment of the receptive field in the skin with subtilisin most C-fibres do not lose mechanosensitivity (Figure 6). However, we also monitored the mechanical latency of the responses during the course of the experiment. Mechanical latency is the time from the onset of the ramp stimulus until the first spike corrected for conduction delay and is a good measure of the mechanical threshold (Milenkovic et al., 2008). In control experiments the mechanical latency of C-fibre responses is always stable with repeated supra-threshold stimuli (Figure 7C). However, in subtilisin-treated C-fibres the mean mechanical latency increased steadily and significantly during the course of the treatment (Figure 7C). The increased mechanical latency in single C-fibres is reminiscent of the increased latency of the mechanosensitive current that we observed after subtilisin/blisterase/furin treatment in vitro (Figure 7A and B). The change in mechanical latency observed in C-fibres after subtilisin was not observed in other afferent fibres including Aδ-mechanonsensitive receptors (AM) (Supplementary Figure S4).

Discussion

In this paper we provide direct evidence that mechanosensitive channels, which underlie vertebrate touch sensation, require an extracellular tether protein to function. Genetic screens for touch-insensitive worms have revealed alleles of the mec genes that encode putative extracellular proteins (Gu et al., 1996; Emtage et al., 2004). Also mutant flies lacking mechanoreceptor potentials harbour mutations in the NompA gene that encodes a large extracellular protein that may be well-positioned to interact with transduction channels in bristle sensory neurons (Chung et al., 2001). However, the extracellular proteins identified in such genetic screens have not been shown to interact directly with transduction channels (Cueva et al., 2007) and may instead play a structural or organizing role (Chung et al., 2001; Emtage et al., 2004). Indeed if such proteins act as gating tethers then acute ablation of the protein should abolish mechanotransduction as demonstrated in vertebrate hair cells (Assad et al., 1991; Zhao et al., 1996; Goodyear and Richardson, 2003; Siemens et al., 2004; Kazmierczak et al., 2007), but such experiments have not yet been conducted using model organisms such as worms and fruit flies.

The situation for mechanoreceptors that mediate touch sensation in vertebrates was unknown. However, here we demonstrate that mechanosensitive currents that are necessary for mechanoreceptor function (see Supplementary Figure S1) only work in the presence of an extracellular subtilisin/blisterase/furin-sensitive protein tether. Thus, under three experimental conditions (acute subtilisin, acute blisterase and in cultured sympathetic ganglion neurons) no or few neurons are recorded with an RA-mechanosensitive current and few or no tethers >75 nm are observed. In contrast, there were three other situations where tethers were observed and so were RA-mechanosensitive currents (control, subtilisin recovery and PIPLC treatment). We were also able to demonstrate that loss of the RA-mechanosensitive current can happen within a few minutes of exposure to the endopeptidase subtilisin (Figure 2A). This striking finding strongly suggests that a subtilisin-sensitive polypeptide is directly involved in maintaining the function of the RA-mechanosensitive current. It might be argued that the functionally important peptides that are cleaved by subtilisin and blisterase are not identical to the ~100-nm-long tether that we have identified in our TEM studies. However, the fact
that non-mechanosensory sympathetic neurons also do not synthesize a 100-nm-long tether protein lends further support to the idea that this entity is functionally relevant for RA-mechanosensitive currents. A further possibility is that the protease treatments we have used here cleave the mechanosensitive channel directly and we cannot exclude such a possibility at the present time. However, we have demonstrated that the function of a variety of voltage-gated and ligand-gated ionic currents was largely unaffected by the protease treatments used (Figure 3), and this includes putative ASIC-like currents that are mediated by ion channels with a very large extracellular polypeptide.

Figure 6 Mechanoreceptors, but not nociceptors, require a subtilisin-sensitive protein. (A) A schematic representation of the recording setup using the in vitro skin-nerve preparation and an example of a recording from a mechanoreceptor (SAM) before (black trace) and after application of subtilisin locally to the receptive field (red trace). Note that the electrically evoked spike is unaffected by the treatment, but the fibre's mechanosensitivity was completely abolished. (B) Kaplan–Meyer plots of the percentage of sensory fibres with a mechanosensitivity before and after local application of subtilisin. The top row contains data from three types of mechanoreceptor (RAM, SAM and D-hair are shown; note that subtilisin abolishes mechanosensitivity in all three receptors, with a median survival time as indicated). The bottom row shows the same experiment for A-fibre nociceptors (AMs) and for nociceptive C-fibres; no significant effect of subtilisin was observed. *** indicates statistical significance (P<0.005 log-rank test).
We show that mechanoreceptor function in vivo is also dependent on a protease-sensitive extracellular polypeptide. The effects of subtilisin treatment on mechanoreceptor function were remarkably specific in that the mechanosensitivity of single mechanoreceptors was rapidly (< 3 min) abolished, but electrical excitability was completely preserved (Figure 6A). So far this is the first example of any treatment, pharmacological or otherwise, that can specifically ablate the mechanosensitivity of cutaneous afferents in vivo. The effects of subtilisin treatment in the intact skin also mirrored those observed in vitro in that nociceptor mechanosensitivity was largely preserved (Figure 2). Interestingly, the mechanical latency of C-fibre nociceptors increased substantially during subtilisin treatment and this phenomenon is reminiscent of the increased latency in the SA-mechanosensitive current observed following subtilisin treatment in vitro (Figure 7). We have previously shown that the mechanical latency of C-fibre nociceptors is surprisingly long as the fastest latency measured in nociceptors remains unexplained. However, it should be noted that the mechanical latency in vivo directly reflects changes in mechanical threshold as well as the speed of transduction. Thus the elevation in mechanical latency observed after subtilisin treatment may accompany a higher threshold for gating of the SA-mechanosensitive current. The mode of mechanical stimulation that we have used here to evoke mechanosensitive currents is usually supra-threshold and so changes in threshold would not necessarily be detected using our experimental design. Together our data suggest that a protease-sensitive extracellular element is involved in regulating the mechanosensitivity of many nociceptors, but is not essential for mechanotransduction in these afferent fibres. However, there remains the possibility that like in the hair cell there are extracellular proteins that are not readily cleaved even by the non-specific protease subtilisin (Osborne and Comis, 1990; Goodyear and Richardson, 1999).

Stretch-activated channels have been characterized in many cell types (Guharay and Sachs, 1984; Lane et al., 1991) and recent evidence suggests that a stretch-activated channel (SAC) is regulated by members of the TRP-channel family (Sharif-Naeni et al., 2009). However, the role of SACs in mechanoreceptors has been controversial (Morris and Horn, 1991; Cho et al., 2002) and our data show that it is unlikely that membrane stretch, by itself, is sufficient to gate mechanosensitive channels required for touch perception. However, it is intriguing that the SA current, found exclusively in nociceptors (Hu and Lewin, 2006; Lechner et al., 2009), appears largely insensitive to extracellular proteolysis both in vitro and in vivo (Figures 2 and 6). Interestingly, at least three types of SACs with different thresholds and single-channel conductance have been recorded by Oh and workers in the membranes of nociceptive sensory neurons (Cho et al, 2002, 2006). It is not clear at the moment whether these SACs underlie the SA-mechanosensitive current that we and others have recorded to direct mechanical stimulation (Drew et al., 2002, 2004, 2007; Hu and Lewin, 2006). Nevertheless, we provide evidence here that the kinetics of the SA-mechanosensitive current is dependent on protease sensitive link to

**Figure 7** Protease modulation of transduction speed. (A) The latency of the SA-mechanosensitive current was measured in controls and protease-treated cells. Note that all protease treatments led to clear increase in the mechanical latency of the current (horizontal lines) as compared with that in the control (black trace), and this recovered to control values after recovery (blue trace bottom). Note that all vertical scale bars denote 100 pA. (B) Quantification of data shown in panel A; all three protease treatments lead to increased latency of the SA-mechanosensitive current. (C) The mechanical latency of C-fibre nociceptors treated at the receptive field with subtilisin is significantly increased following the application in the skin-nerve preparation. Statistical significance was calculated by repeated-measures ANOVA.
the extracellular matrix (Figure 7). It may be that protease-sensitive extracellular links to SACs or related channels have a primary role in increasing the speed of mechanoelectric transduction, and this interpretation would be supported by our data (Figure 7).

The protein filament that we have identified is synthesized by sensory neurons and appears to have a constant length of ~100 nm and can bind at one end to laminin/nidogen complexes. Indeed we have observed protein tethers in sensory neurons cultured on highly purified laminin-111 (data not shown), a substrate that fully supports the RA-mechanosensitive current (Figure 2). We cannot at the moment say whether the tether we have identified morphologically is a single protein or a multimeric complex like the hair cell tip link (Ahmed et al., 2006; Kazmierczak et al., 2007). Nevertheless, our quantitative TEM data indicates that the filamentous objects >75 nm are remarkably homogenous in terms of size (mean 99 ± 18 nm standard deviation, from all measurements made) despite being measured in ultrathin sections in which its orientation is necessarily variable. Assuming that the protein tether that we have identified anatomically is necessary for activation of the RA-mechanosensitive then we can conclude that this tether does not share any biochemical characteristics with tip-link proteins in hair cells. The protein tether identified here is laminin binding, subtilisin-sensitive and Ca\(^{2+}\)-ion-independent, all features not shared by the hair cell tip link. Importantly, the extracellular part of the protein we have identified must contain at least one blisterase/furin consensus site, both cadherin-23 and protocadherin-15 do not contain such a consensus site, (Puntervoll et al., 2006; Hughey et al., 2007), and protocadherin-15 (data not shown), a substrate that fully supports the RA-mechanosensitive current (Figure 2).

Whole-cell patch-clamp recordings from isolated DRG neurons

Materials and methods

Whole-cell patch-clamp recordings from isolated DRG neurons

Whole-cell recordings were made from DRG neurons using fire-polished glass electrodes with a resistance of 3–5 MΩ. The extracellular solution contained (in mM) 140 NaCl, 1 MgCl\(_2\), 2 CaCl\(_2\), 4 KCl, 4 glucose, 10 HEPES, pH 7.4, and the electrodes were filled with a solution containing (in mM) 122 KCl, 10 NaCl, 1 MgCl\(_2\), 1 EGTA, 10 HEPES, pH 7.3. For most experiments, 0.1% Lucifer Yellow was included in the electrode. The cells were perfused with drug-containing solutions by moving an array of outlets in front of the patched cells (WAS02; Ditel, Prague). TTX was prepared in a final concentration of 1 μM in extracellular solution.

Observations were made using a Zeiss Axiovert 200 microscope equipped with a TILL imaging system, including the polychrome V, a CCD camera and the imaging software TILLvision. Membrane current and voltage were amplified and acquired using an EPC-10 amplifier sampled at 40 kHz; acquired traces were analyzed using the Patchmaster and Fitmaster software (HEKA). For most experiments the membrane voltage was held at −60 mV with the voltage-clamp circuit.

Mechanical stimuli were applied using a heat-polished glass pipette (tip diameter 2–5 μm), driven by a MM3A Micromanipulator system (Kleindiek), positioned at an angle of 45 degrees to the surface of the dish. There are two different movements for the Nanomotor\(^\text{\textregistered}\): 'fine mode' and 'coarse mode'. Fine mode movement from any position is limited to about 740 nm in each direction from the Z-axis (calibrated by a Piezo actuator calibration device LL10PZT; LASERTEX). Coarse mode steps (one step about 750 nm) can be executed in any direction until the micromanipulator reaches its physical limits. The probe was positioned near the neurite or cell body, moved forward in steps of 200–750 nm for 500 ms and then withdrawn. If there was no response, the probe was moved forward by one step coarse mode; the same procedure was repeated until a mechanically activated inward current was recorded. The probe was moved at a speed of 1.4 μm s\(^{-1}\) for the fine mode and 7.5 μm s\(^{-1}\) for the coarse mode. For analysis of the kinetics of mechanoelectric transduction, inward current traces were fit with single exponential functions using the Fitmaster software (HEKA). Data are presented as mean ± s.e.m.

Electron microscopy

DRG or SCG neurons were isolated and cultivated on laminin-coated petriPERM dishes using standard culture conditions (Hu and Lewin, 2006) (petriPERM35; Vivascience AG, Germany). After 24 h, cells were washed twice with 0.1 M cacodylate buffer (Electron Microscopy Sciences, PA, USA), fixed in 2.5% glutaraldehyde for 4 h and stained with osmium tetroxide (Sigma-Aldrich Co. Ltd.) in the presence of ruthenium red (Fluka) to enhance the electron density of extracellular proteins (Hasko and Richardson, 1988). The fixed samples were dehydrated through a series of ethanol exchanges and infiltrated in a mixture of epoxy resin and propylene oxide (Polysciences Inc., Warington, PA, USA) then embedded in a mixture of epoxy resin. The embedded samples were randomly sectioned (50 nm thick) and then contrasted with uranyl acetate and lead citrate (Serva, Germany), and examined with a Zeiss 910 electron microscope. Digital micrographs were taken with a 1k x 1k high-speed, slow-scan CCD camera (Proscan) and analysed with the TEM software (Olympus Soft Imaging Solutions, Münster, Germany). To quantify electron-dense objects under different experimental conditions, microscopic fields were randomly photographed from at least 3–4 cultures in each group and the number and length of electron-dense objects that linked the neurite membrane to the laminin substrate were measured. The sum of the measured area of membrane contact was determined by the sum of the product of neurite contact zone width and the thickness of each ultrathin section. To generate the presentation of raw data as dot clouds, the length of each object was randomly plotted in two-dimensional space. To quantify the average interface distance between the neurite membrane and the laminin substrate, the ratio of interface area (nm\(^2\)) and neurite width along the contact zone (nm) was calculated from each electron micrograph.

Cell culture

The fibroblast cell line (mouse NIH 3T3 cells) was maintained in Dulbecco’s modified Eagle’s medium (DMEM), supplemented with 10% foetal bovine serum, penicillin, streptomycin and glutamine. Confluent cells were sub-cultured each week. Excess cells were irradiated as a suspension with 60 Gy (6000 rads) \(\gamma\)-irradiation. DRG neurons from adult mouse were prepared as described previously (Mannsfeldt et al., 1999; Stucky et al., 2002). No nerve growth factor or other neurotrophin was added to the medium. When co-cultured with 3T3 cells, DRG neurons were irradiated as a suspension with 60 Gy (6000 rads) \(\gamma\)-irradiation. DRG neurons from adult mouse were prepared as described previously (Mannsfeldt et al., 1999; Stucky et al., 2002). No nerve growth factor or other neurotrophin was added to the medium. When co-cultured with 3T3 cells, DRG neurons were irradiated as a suspension with 60 Gy (6000 rads) \(\gamma\)-irradiation. DRG neurons from adult mouse were prepared as described previously (Mannsfeldt et al., 1999; Stucky et al., 2002). No nerve growth factor or other neurotrophin was added to the medium.
plated on top of the 3T3 monolayer instead of on PLL/laminin substrate. All the culture treatments were applied at least 16 h following plating after neurite outgrowth was established. DRG neurons were treated with CD29 (20 µg ml⁻¹, 90–270 min, 37 °C), or PIPLC (25 U ml⁻¹, 120 min, 37 °C) or BAFTA (5 mM, 30 min, 37 °C), immediately following these various treatments, neurons were prepared for whole-cell patch-clamp recordings and the presence or absence of mechanosensitive currents was measured (nominally between 0 and 3 h following treatment). Normally, the first recorded cells were obtained within the first 10 min following placement of the cells in the recording chamber.

Supplementary data
Supplementary data are available at The EMBO Journal Online (http://www.embojournal.org).

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Conflict of interest
The authors declare that they have no conflict of interest.
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