Research Article

Emotion Analysis of College Students Using a Fuzzy Support Vector Machine

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1. Introduction

On contemporary university campuses, the number of college students with mental illnesses is increasing day by day. Many college students have difficulty adapting to college life for a while, and a series of mental health problems arise, which seriously affect their normal study and life. At present, the mental health prevention work of college students mainly relies on the inquiry methods of counselors and class teachers. The problems with this approach are as follows. (1) The number of teachers is far lower than the number of potential mental health problems. In addition, the work of university teachers is complicated, and the workload is huge, with limited energy and time. Therefore, the prevention and treatment of mental health among college students are often a mere formality. (2) At present, the main way to carry out mental health prevention and control work is questionnaire survey, which is difficult to identify students with real psychological problems. This has given birth to more intelligent mental health investigation and prevention methods. The emotional changes of college students can reflect their mental health problems to a certain extent. If a college student is in a sad or neutral state for a long time, it indicates that the student has some psychological problems. At this time, the teacher can start mental health counseling in time. Therefore, emotion recognition for college students is of great significance.
Emotion is a very complex psychological state produced by human beings in a specific environment, which is often associated with temperament, temperament, and motivation [1]. People can feel their own emotional state at all times; it provides a guarantee for human survival, and affects our learning, decision-making, and memory capabilities [2]. Emotion is a person’s attitude and experience towards objective situations or things. It is a physical and psychological state produced by a person’s senses, thoughts, and behaviors [3]. Emotion occupies an important position in the human society. As an advanced function of the human brain, it can ensure the adaptability of people in different environments. At the same time, it can characterize human personality characteristics and psychopathology [4]. Generally, positive emotions can make people full of strength and vitality and make people energetic, so it is beneficial to physical and mental health and the recovery of the body. Neutral emotion is an important criterion for personal psychological stability. Negative emotions usually cause a person to become depressed. Being in this state for a long time will affect people’s working conditions and endanger physical and mental health.

Therefore, emotion recognition and monitoring has become a necessary way to solve human mental illness. Human emotion prediction also has important research significance and application value in areas such as mental health evaluation. For example, in medicine, the relationship between emotion and stress and other diseases is studied by analyzing physiological signals such as EEG in different emotional states [5, 6]. It is possible to find new ways to treat and recover similar mental illnesses. In education, the distance teaching platform based on emotion recognition can become more humane by obtaining feedback from students [7]. In entertainment, intelligent emotional sensing robots can bring more fun to life. With the deepening of research on emotion recognition, its service areas for humans will become more extensive. At present, in terms of research materials, emotion recognition can be divided into speech-based [8, 9], video-based [10, 11], image-based [12–14], text-based [15, 16], and physiological signal [17, 18] and emotion recognition [19, 20] combining multiple modal data. In the recognition of classifiers, they are mainly based on machine learning [21–28] and based on deep learning [29, 30]. Machine learning algorithms have been successfully applied to the recognition of various physiological signals [31–36]. The application of deep learning algorithms is still being explored further.

This article is mainly devoted to the research of emotion recognition based on EEG signals. In sentiment analysis based on EEG signals, there are mainly two methods. They are linear analysis method and nonlinear analysis method. Representative studies are shown in Table 1.

The abovementioned EEG-based emotion recognition method does not consider the characteristics of different rhythms in the EEG signal but processes the EEG uniformly. This method ignores the different effects of different rhythms on emotion recognition. Aiming at this problem, this paper proposes an emotion recognition method based on the fusion of multiple rhythm results. The contributions of this research are summarized as follows:

1. In order to fully excavate the information characteristics of different rhythms in EEG signals, this paper extracts and classifies multiple rhythms. This method can make full use of the information of different rhythms and has better pertinence.

2. Aiming at the problem of large feature dimension space and difficulty in integrating multiple rhythms in emotion recognition, in this study, the D-S evidence combination theory was used to merge multiple rhythm classification results to obtain the final classification results. The result fusion method can not only obtain more accurate results than a single rhythm or simple integration of multiple rhythms but also reduce the dimension of the feature space and overcome the problem of how to integrate multiple rhythms.

3. This study used the FSVM classifier. Due to the introduction of the fuzzy membership mechanism, this classifier has better noise immunity than other classic classifiers. This classifier is more suitable for applications in noisy actual production environments.

2. Emotion Recognition Based on EEG Signals

2.1. Emotion Recognition Process Based on EEG Signal. The process of emotion recognition is essentially a process of pattern recognition, which is generally divided into three steps. They are data collection and preprocessing, feature extraction, and model training and recognition. Figure 1 is a flowchart of emotion recognition. In the supervised machine learning process, it is first necessary to label the acquired sample set, divide it into different categories, and divide the sample set into training set and test set. Secondly, data preprocessing and feature extraction are required for the two sets. Finally, train the model by the training set. The trained model is for classification and decision-making. In the recognition process, the test set features are sent to the trained model for sample prediction. The output emotion category label is the recognition result, thus completing the whole process of emotion recognition.

2.2. Introduction to EEG Signals. According to different classification basis, EEG signals can be divided into categories as shown in Table 2.

In the preprocessing of the received EEG signal, noise reduction processing is mainly performed. At the same time, it reduces the interference of non-brain wave signals such as skin electricity and muscle electricity. Then feature extraction is performed on the data to obtain useful signals for sentiment analysis.

2.3. Feature Extraction of EEG Signals. In this study, the wavelet transform was used to extract 4 rhythms in EEG electrode signals, namely, $\theta$ rhythm, $\alpha$ rhythm, $\beta$ rhythm, and $\gamma$ rhythm. Taking $\beta$ as an example, calculate the wavelet packet coefficients of the $\beta$ wave decomposition node of the
Table 1: Representative research on emotion recognition based on EEG signals.

| Method                                                                 | Feature                                                                 | Representative research | Recognition rate (%) |
|------------------------------------------------------------------------|-------------------------------------------------------------------------|-------------------------|----------------------|
| Linear analysis methods (Pearson correlation, amplitude squared coherence, autoregressive model, cumulative energy algorithm, time-frequency analysis, etc.) | EEG signal waveform characteristics (such as amplitude, phase, etc.), rhythm wave average power, power spectral density, band energy, wavelet coefficient root mean square, etc. | References [6] | 60.42 |
| Nonlinear analysis methods (mutual information [38], correlation dimension, Lempel–Ziv (LZ) complexity, recursive graph, and entropy analysis [39]) | Entropy, fractal dimension, correlation dimension, CO complexity, LZ complexity, Hust index, maximum Lyapunov index, etc. | References [37] | 88.51 |

Table 2: Classification of EEG signals.

| Classification basis | Classification details |
|----------------------|------------------------|
| Frequency            | (1) $\delta$ (0.1–4 Hz) |
|                      | (2) $\theta$ (4–8 Hz) |
|                      | (3) $\alpha$ (8–13 Hz) |
|                      | (4) $\beta$ (13–30 Hz) |
|                      | (5) $\gamma$ (31–100 Hz) |
EEG signal and obtain various statistical values of the EEG signal through calculation. These original statistical values are used as original features. According to the particularity and difference of the EEG signal, the average energy of the $\beta$ wave rhythm of the EEG signal in the time domain and the frequency domain is extracted. The characteristics of the extracted $\beta$ waves are shown in Table 3.

The calculation formula of some statistical values is as follows:

\[
\begin{align*}
\text{mean} &= \frac{1}{N} \sum_{n=1}^{N} E_n, \\
\text{std} &= \sqrt{\frac{1}{N-1} \sum_{n=1}^{N} (E_n - \text{mean})^2}, \\
\min \text{Ratio} &= \frac{\min N}, \\
\max \text{Ratio} &= \frac{\max N}, \\
\text{Energy Mean} &= \frac{1}{N} \sum_{n=1}^{N} E_n^2,
\end{align*}
\]

where $E$ represents the brain electrical signal data and $N$ represents the length of the brain electrical signal data.

**2.4. Learning and Classification of EEG Signals.** A support vector machine (SVM) is one of the most common classification methods in emotion recognition. Considering that the classic SVM is susceptible to noise interference, the EEG signal collected in the real production environment usually contains noise interference. In order to improve the classification accuracy, this paper uses the SVM with fuzzy membership.

Let the training sample set be $\{x_i, y_i, u(x_i)\}_{i=1}^{N}$. $x_i$ represents the feature vector of each sample. $y_i$ represents two different categories, $y_i \in \{+1, -1\}$. $u(x_i)$ is the fuzzy membership function. $u(x_i)$ represents the membership degree of the $i$th sample and represents the reliability of the $i$th sample $x_i$ belonging to the $y_i$ class, $0 < u(x_i) \leq 1$. According to the principle of the SVM algorithm, the training samples are mapped to the high-dimensional feature space, and the feature mapping function $\phi(\cdot)$ is used to obtain $\mathbb{R}^d \rightarrow \mathbb{R}^p$. The training sample is converted to $\{\phi(x_i), y_i, u(x_i)\}$. The classification hyperplane is $w^* \phi(x_i) + b = 0$, where $w$ is the kernel function represented by $\phi(\cdot)$ and is $K(x_i, x_j) = \phi(x_i)^T \phi(x_j)$.

\[
\begin{align*}
\min & \quad \frac{1}{2} \|w\|^2 + C^+ \sum_{\{i=1\mid y_i=+1\}} u_i^+ \xi_i + C^- \sum_{\{i=1\mid y_i=-1\}} u_i^- \xi_i \\
\text{s.t.} & \quad y_i [w \cdot \phi(x_i) + b] - 1 + \xi_i \geq 0, \quad i = 1, 2, \ldots, n \quad (1)
\end{align*}
\]

where $C^+$ and $C^-$ represent the penalty factors of positive and negative samples, respectively. $\xi$ is the relaxation factor. The optimal hyperplane is obtained by solving the objective function by the Lagrangian multiplier method:

\[
\begin{align*}
f(x) = \text{sgn} \left( \sum \alpha_i y_i K(x_i, x) + b \right). \quad (3)
\end{align*}
\]

According to the degree of influence of each sample on the classification surface, each sample point is given a different degree of membership. The purpose is to make the sample points with larger influence degree have a larger degree of membership, and the sample data with smaller effect will give a smaller degree of membership.

**2.5. The D-S Evidence Combination Theory.** Dempster first described the Dempster–Shafer evidence combination theory in his article [43]. Later, Shafer further developed and perfected the theory, which formed the Dempster–Shafer evidence combination theory as it is now known. The Dempster–Shafer evidence combination theory is also called the D-S evidence theory. It expands the data fusion solution and is widely used in multisource data fusion. The D-S evidence theory is based on the trust function of different observations and uses Dempster’s evidence combination.
rules to fuse them. Then a judgment is made on the result obtained according to a certain type of rule, and finally the fusion and final decision result is realized. The principle is described as follows [44].

Suppose a finite space $\Theta$ and let $\mathcal{P}$ be all the subsets in the space $\Theta$. This also includes the empty set $\Theta$ itself. For the subset $A$, define the function $m: \mathcal{P} \rightarrow (0, 1)$ and satisfy

$$
\sum_{A \subseteq \Theta} m(A) = 1,
$$

$$
\left\{ \begin{array}{l}
m(\Theta) = 0. \end{array} \right. \quad (4)
$$

Function $m(A)$ is the basic confidence distribution function on $\Theta$, and $m(A)$ is the precise trust level of the subset $A$. In this theory, the basic confidence distribution function is assigned to $A$ in a fixed form as its evidence information. However, different people will give inconsistent confidence assignments to the same evidence because of their special experience and knowledge. Maximize the use of independent and different sources of evidence to improve the accuracy or confidence of the target event.

$$
m(D) = \frac{1}{k} \sum_{A \cap B = D} m_1(A)m_2(B). \quad (5)
$$

Assume

$$
m(\Phi) = 0, k = 1 - \sum_{A \cap B = \Phi} m_1(A)m_2(B). \quad (6)
$$

### 3. The Proposed Emotion Recognition Method

Different rhythms in EEG data correspond to different emotional states, because emotion recognition based on a single rhythm often has problems such as low recognition rate and poor stability. Using multiple EEG rhythms as feature recognition will improve the recognition results and stability. At present, most emotion recognition based on multiple EEG rhythms simply combine the feature recognition results extracted from these rhythms, and there is no more effective fusion strategy. This makes the dimension of the feature space and the input dimension of the classifier too high, making the accuracy and stability of the discrimination result poor. In order to make full use of the advantages of EEG data and improve decision-making results, this study applies the D-S theory to the decision-making level. The main idea of the proposed method is: First, extract the four characteristic rhythms in the EEG electrode signal: $\theta$ rhythm, $\alpha$ rhythm, $\beta$ rhythm, and $\gamma$ rhythm, and extract each characteristic wave separately. Secondly, input the feature vector into the corresponding FSVM classifier for recognition. Finally, the basic confidence distribution of each mode under each classifier is obtained, and the D-S evidence combination theory is used to fuse the classification results to obtain the final decision result. The framework of the proposed method is shown in Figure 2.

The steps of the proposed algorithm are as follows:

1. Step 1: prepare the electrodes FC5-FC6 to be analyzed, respectively. Due to the time-varying nonstationary characteristics of EEG, preprocessing is essential before waveform extraction. Among them, there are mainly framing and windowing. Set the frame length to 512, the frame shift to 256, and the window function to the hamming window.
2. Step 2: extract the $\theta$ rhythm, $\alpha$ rhythm, $\beta$ rhythm, and $\gamma$ rhythm of each electrode signal after preprocessing, and use them as the EEG characteristic band. The feature extraction is shown in Table 4.
3. Step 3: assign an FSVM classifier to identify each rhythm. Each FSVM can be regarded as independent evidence, and its output value is transformed into the basic confidence function of each emotion model under evidence.
4. Step 4: after obtaining the basic allocation function of each FSVM classifier in step 3, perform fusion according to the formula (5).
5. Step 5: the fusion result is judged according to the rules: $m(A_w) = \max(m(A_i))$, the function with the maximum trust degree is selected as the target class.

### 4. Experiment Analysis

#### 4.1. Experimental Data and Parameter Settings

The data set used in this study is a public data set provided by S. Koelstra et al. for analyzing the human emotional state. The data set contains audio and video, 32-lead EEG data and 8-lead peripheral physiological signals. The data set is divided into 4 emotions, namely, high arousal and high valence (HAHV), low arousal and high valence (LAHV), low arousal and low valence (LALV), and high arousal and low valence (HALV).

In the experiment, 312 training samples were selected and 144 test samples were selected. Each type has 78 training samples and 36 test samples. This study used the data that were preprocessed by experimenters such as S. Koelstra and others.

### Table 3: Abbreviations and descriptions of signal statistical characteristics.

| Feature abbreviations | Description                                      |
|-----------------------|--------------------------------------------------|
| Mean                  | The average value of the $\beta$ wave            |
| Median                | Median of the $\beta$ wave                       |
| Std                   | Standard deviation of the $\beta$ wave           |
| Min                   | Minimum value of the $\beta$ wave                |
| Max                   | Maximum value of $\beta$ wave                    |
| Min Ratio             | The ratio of the minimum number of $\beta$ waves to the signal length |
| Max Ratio             | The ratio of the maximum number of $\beta$ waves to the signal length |
| Energy Mean           | Average energy of $\beta$ wave                   |

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| Energy Mean           | Average energy of $\beta$ wave                   |

Assume

$$
m(\Phi) = 0, k = 1 - \sum_{A \cap B = \Phi} m_1(A)m_2(B). \quad (6)
$$
others after removing oculogram, frequency reduction, and filtering from the original data. The data sampling frequency of each segment is reduced to 128 Hz, and the sampling time is 63 seconds. The first 3 seconds are the baseline duration, and the next 60 seconds are the experimental data.

The contrast classifiers used in this study are SVM, Gaussian mixture model (GMM), and BP neural network (BPNN). The parameter $c \in \{2^{-5}, \ldots, 2^5\}$ and nuclear parameter $\gamma \in \{2^{-5}, \ldots, 2^5\}$. The number of Gaussian components is 6. The evaluation index is the recognition rate.

4.2. Experimental Program and Result Analysis. This study designed experiments from three perspectives: single multirhythm as data input, different classification result fusion strategies, and different classifiers. The specific design plan is as follows:

Scheme 1: In order to verify the influence of single multirhythm as data input on emotion recognition, the experiment compared the recognition rate of single rhythm and multirhythm in different combinations. The multirhythm classification result of this experiment uses the fusion of the D-S evidence combination theory, and the classifier uses the FSVM. The experimental results are shown in Table 5 and Figure 3.

Scheme 2: In order to verify the effectiveness of the D-S fusion strategy used, the two result fusion methods of ordinary linear combination and D-S evidence combination are compared. The experimental data use a combination of $\alpha + \beta + \gamma$ three rhythms. The experimental results are shown in Table 6.

Scheme 3: In order to verify the robustness of the FSVM classifier, the classic SVM, GMM, and BPNN are selected for the comparison classifier. The experimental result data are a multirhythm fusion classification result. The experimental results are shown in Table 7 and Figure 4.

From Table 5 and Figure 3, the following conclusions can be drawn:

1. In a single rhythm, the recognition rate of different rhythms is different. It shows that the contribution of information carried by different rhythms is different. Among them, rhythms $\beta$ and $\gamma$ have the better recognition rate, which shows that rhythms $\beta$ and $\gamma$ can truly reflect emotional changes. When performing multifeature recognition, these two kinds of rhythms should be given priority.

2. The recognition rate of different combinations of each rhythm is higher than that of any single rhythm. This shows that emotion recognition performance based on multiple rhythm combinations is better. Among the multirhythms of different combinations, the D-S fusion recognition rate of the three rhythms $\alpha + \beta + \gamma$ is the highest. The fusion recognition rate of the four rhythms $\theta + \alpha + \beta + \gamma$ is lower than the fusion recognition rate of the three rhythms $\alpha + \beta + \gamma$.
Table 5: Comparison of the recognition rate between single rhythm and multirhythm recognition.

| Rhythm          | HALV | LAHV | LALV | HALV | Mean |
|-----------------|------|------|------|------|------|
| Single rhythm   |      |      |      |      |      |
| $\theta$        | 0.5280 | 0.5426 | 0.4985 | 0.5446 | 0.5284 |
| $\alpha$        | 0.5390 | 0.5566 | 0.5078 | 0.5335 | 0.5342 |
| $\beta$         | 0.5618 | 0.6309 | 0.4775 | 0.5821 | 0.5631 |
| $\gamma$        | 0.5885 | 0.5321 | 0.5347 | 0.5538 | 0.5523 |
| $\theta + \alpha$ | 0.5311 | 0.5489 | 0.5026 | 0.5523 | 0.5337 |
| $\theta + \beta$ | 0.5602 | 0.6243 | 0.4724 | 0.5953 | 0.5631 |
| $\theta + \gamma$ | 0.5925 | 0.5341 | 0.5387 | 0.5622 | 0.5569 |
| $\alpha + \beta$ | 0.5454 | 0.6243 | 0.4856 | 0.5754 | 0.5577 |
| $\alpha + \gamma$ | 0.5565 | 0.5287 | 0.5295 | 0.5432 | 0.5395 |
| Multirhythm fusion |      |      |      |      |      |
| $\beta + \gamma$ | 0.5743 | 0.6265 | 0.5043 | 0.5754 | 0.5701 |
| $\theta + \alpha + \beta$ | 0.6117 | 0.5876 | 0.5906 | 0.5350 | 0.5812 |
| $\theta + \alpha + \gamma$ | 0.6243 | 0.5973 | 0.5667 | 0.5465 | 0.5837 |
| $\alpha + \beta + \gamma$ | 0.7088 | 0.5630 | 0.5894 | 0.6421 | 0.6258 |
| $\theta + \alpha + \beta + \gamma$ | 0.7008 | 0.5534 | 0.5878 | 0.6346 | 0.6192 |

Figure 3: Continued.
This shows that it is not that more rhythms are better. Some rhythms carry less useful information, which will weaken the final decision result. The recognition rate of any combination of two rhythms is lower than the recognition rate of $\alpha + \beta + \gamma$ three rhythm combinations. Among the three rhythm combinations, the recognition rate of $\alpha + \beta + \gamma$ three rhythm combinations is significantly higher than the other three rhythm combinations. This shows that in order to obtain the optimal decision result, not only the number of combined rhythms must be confirmed but also the most representative rhythm must be selected.

It can be concluded from Table 6 that the fusion method based on the D-S evidence combination has the highest recognition rate. The separate discrimination results of the three rhythms are merged, and the group with the largest trust degree after fusion is taken as the target class. The linear combination experiment simply integrates the three rhythm features into a set of feature vectors. In the process of pattern recognition, misjudgment may be caused due to the inconsistency between certain dimensional features. From the comparison of these two sets of experiments, it can be concluded that the D-S evidence combination theory can reduce the misjudgment caused by the inconsistency between the features to a certain extent, thereby improving the recognition rate.

From Table 7 and Figure 4, the following conclusions can be drawn: the emotion recognition rate under the FSVM classifier is the highest. It is 3.02% higher than SVM, 3.47% higher than GMM, and 1.33% higher than BPNN. The overall improvement is not large, which shows that the use of different classifiers has little effect on the final recognition rate. Among different classifiers, the recognition rates of BPNN and FSVM are not much different. This shows that although the neural network-based classifier has high computational time complexity, the final decision-making effect is ideal. For some operations that do not consider time cost, we can consider using a neural network-based classifier. By comparing the four emotion recognition results, we
found that the recognition rates of HALV and HALV are generally higher. Divided from the degree of arousal, both categories belong to the range of high arousal. This shows that EEG emotional data with high arousal have a better performance in recognition.

5. Conclusion

As the pressure of college students increases, some negative events occur frequently. Emotion recognition for college students is particularly important and meaningful. In this context, this article proposes an EEG signal-based emotion recognition method for college students. First of all, in the use of data sets, this study uses multirhythms as data input. Through experimental comparison, three rhythms were finally selected. The second step is to use the wavelet transform for feature extraction for each rhythm. The third step is to use the FSVM classifier to classify the input feature data to obtain classification results of different rhythms. The fourth step is to use the D-S evidence combination theory to fuse the classification results of the three rhythms, to get the final decision result. There are 3 points of innovation in this research. One is to use multiple rhythms as input. The second is to introduce the FSVM classifier with strong noise immunity. The third is to use the result fusion strategy based on the D-S evidence theory. Through experimental comparison, the emotion recognition method proposed in this article can effectively improve the recognition rate, which has a reference value. However, this study also has some shortcomings; for example, classifying different rhythms separately; this method directly discards the relationship between different rhythms and may reduce the final recognition effect. Subsequently, a classifier based on a collaborative learning mechanism is used for classification and recognition.

Data Availability

The data used to support the findings of this study are available from the corresponding author upon request.

Conflicts of Interest

The authors declare that they have no conflicts of interest.

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