Comparison of prostate contours between conventional stepping transverse imaging and Twister-based sagittal imaging in permanent interstitial prostate brachytherapy

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Abstract

Purpose: To compare prostate contours on conventional stepping transverse image acquisitions with those on twister-based sagittal image acquisitions.

Material and methods: Twenty prostate cancer patients who were planned to have permanent interstitial prostate brachytherapy were prospectively accrued. A transrectal ultrasonography probe was inserted, with the patient in lithotomy position. Transverse images were obtained with stepping movement of the transverse transducer. In the same patient, sagittal images were also obtained through rotation of the sagittal transducer using the “Twister” mode. The differences of prostate size among the two types of image acquisitions were compared. The relationships among the difference of the two types of image acquisitions, dose-volume histogram (DVH) parameters on the post-implant computed tomography (CT) analysis, as well as other factors were analyzed.

Results: The sagittal image acquisitions showed a larger prostate size compared to the transverse image acquisitions especially in the anterior-posterior (AP) direction (p < 0.05). Interestingly, relative size of prostate apex in AP direction in sagittal image acquisitions compared to that in transverse image acquisitions was correlated to DVH parameters such as D90 (R = 0.518, p = 0.019), and V100 (R = 0.598, p = 0.005).

Conclusions: There were small but significant differences in the prostate contours between the transverse and the sagittal planning image acquisitions. Furthermore, our study suggested that the differences between the two types of image acquisitions might correlated to dosimetric results on CT analysis.

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addition, the relationships among the difference of the two types of image acquisitions, the dose-volume-histogram (DVH) parameters on the post-implant CT analysis, as well as other factors were analyzed.

Material and methods

Patients

The Institutional Review Board approved this prospective study (B14-60). Written informed consent was obtained from all 20 patients who participated in this study. Eligible participants were adults > 20-years-old with localized prostate cancer, clinical stage T1c-T2c, with prostate-specific antigen (PSA) level < 20 ng/mL, and Gleason score ≤ 8. Exclusion criteria included any contraindications for anesthesia or need for additional external radiotherapy, and refusal to participate. Seven patients had neoadjuvant hormonal therapy. Median duration of hormonal therapy was 5.5 months (range, 4-35 months). The patients’ characteristics are shown in Table 1.

Image acquisition

A TRUS probe (HI VISION Preirus, Hitachi Aloka Medical, Ltd., Tokyo, Japan) was inserted, with the patient in the lithotomy position. Transverse images were acquired through the stepping movement of the transverse transducer set at the tip of the TRUS probe with 1 mm spacing. In addition, sagittal images of the same prostate were acquired through rotation of the TRUS probe using the Twister mode. These two types of images from each patient were then imported into the planning software and were reconstructed into 3-dimensional volume data. All of these image acquisitions were done before needle insertion. The resolution of TRUS images along with X, Y, Z axis were 0.011 cm, 0.011 cm, and 0.100 cm, respectively, for both types of image acquisitions. Quality assurance and quality control of our ultrasound system was performed according to Japanese guideline for seed implantation [3] that was made referring to reports form of American Association of Physicists in Medicine (AAPM) task group.

Prostate size measurements

Prostates were independently contoured by 2 radiation oncologists and 1 urologist (S.K., H.I., and H.T.) on each slice of transverse image or each transverse plane of the reconstructed 3-dimensional volume data (1 mm slice thickness). Urethra, rectum, and seminal vesicles were not contoured. The investigators could refer to sagittal and coronal plane when they contoured the prostate on transverse plane.

The contoured prostate size was measured in the anterior-posterior (AP) direction at 1) the apex, 2) the mid-gland, and 3) the base; in the left-right (LR) direction at 4) the apex, 5) the mid-gland, and 6) the base; and in 7) the superior-inferior (SI) direction. In addition, the distances from the probe surface to the anterior prostate edge were measured at 8) the apex, 9) the mid-gland, and 10) the base (Figure 1). The base and the apex were defined as the first and last contoured slice on the image set, and the mid-gland was defined as the slice at midpoint between the two. The volume of contoured prostate were automatically calculated by the software. These measurements were compared between the transverse and the sagittal image acquisitions. The mean values of 3 investigators’ measurements were used as the sizes of each prostate. Inter-observer variation was defined as each difference from the mean value of 3 investigators.

Treatment

An interactive planning technique was used for all patients [4]. After peripheral needle insertion, a transverse TRUS image was acquired again. If needed, the prostate contour was modified based on the second TRUS image because of swelling and deformation of the prostate due to needle insertion. After implantation of radioactive sources with peripheral needles, the interior needles were inserted and the remaining radioactive sources were implanted. If required, the dosimetry was modified based on real-time dose calculation during the procedure.

All treatments were planned only on transverse images using the planning software. The prescribed dose to the prostate was 145 Gy, with a 3- to 5-mm margin. Two types of 125I source were used: either OncoSeed® model 6711 (GE Healthcare [Medi-Physics], Inc, Arlington Heights, IL, USA), or BrachySource® model STM125I (CR BARD, Murray Hill, NJ, USA). Source activities were 11.0 MBq or 13.1 MBq. Both free sources and intraopera-

Table 1. Patients’ characteristics

| Age (y) | 69 (7.2) |
| T stage | |
| 1c | 7 |
| 3a | 7 |
| 2b | 3 |
| 2c | 3 |
| iPSA (ng/ml) | 6.73 (1.75) |
| Gleason score | |
| 3+3 | 9 |
| 3+4 | 4 |
| 4+3 | 5 |
| 4+4 | 2 |
| Hormonal therapy | |
| Yes | 7 |
| No | 13 |
| Height (cm) | 165.9 (5.8) |
| Weight (kg) | 63.4 (8.4) |
| BMI | 23.0 (3.0) |

Values are given as means (standard deviation) or numbers
iPSA – initial prostate-specific antigen, BMI – body mass index
tively built custom-linked (IBCL) sources were used for patients in this study. The free sources were placed one by one transperineally with needles attached to a Mick applicator (Eckert & Ziegler BEBIG, Berlin, Germany). The IBCL sources were connected to each other using the QUICKLINK system (CR BARD, Murray Hill, NJ, USA) and inserted through a relay system [5]. It has been reported that there is no dosimetric difference between free sources and IBCL sources [6].

**DVH analysis**

Post-implant computed tomography (CT) analysis was completed for all patients based on conventional CT images with 1.25 mm slice thickness acquired 1 day and 1 month after implantation. In this study, all structures except the urethra were contoured based on the 1 month CT. On the 1 day CT, the outer rim of the urethral catheter was contoured as the urethra. The rectal wall, including the sphincter muscle, was fully contoured on the CT images. The urethra and rectum were contoured in the same slices as the prostate contour. The DVH parameters collected from the CT analysis included the dose to 90% of the prostate volume (pD90); the prostate volume receiving at least 100% of the dose (pV100); the prostate volume receiving at least 150% of the dose (pV150); the urethral volume receiving at least 150% of the dose (uV150); the dose to 30% of the urethral volume (uD30); the dose to 5% of the urethral volume (uD5); the rectal volume receiving at least 100% of the dose (rV100); and the rectal volume receiving at least 150% of the dose (rV150).

**A phantom study**

To deny the possibility of image acquisitions themselves causing some differences of prostate size, a phantom study was completed. The in-house oval sphere shaped phantom was set in a tank of water (Figure 2), and was scanned by TRUS using the same methodology as in the above-mentioned human study. CT scan with 1.25 mm slice thickness was also done for the phantom.

**Statistical analysis**

Statistical analyses were performed using R software, version 3.2.0. (R Foundation, Vienna, Austria). The paired t-test was used for comparison of the prostate size between the two types of image acquisitions. Pearson’s correlation coefficients were calculated for the DVH parameters,
the differences of the two types of image acquisitions, and
the patients’ characteristics including body mass index
(BMI), age, and with or without hormonal therapy.

Results

Figure 3 shows a representative case with contours
overlaid based on the transverse and sagittal image ac-
quisions. There was an apparent difference between the
transverse-based and the sagittal-based contours. Table 2
shows the comparison of prostate size between the two
types of image acquisitions. In the sagittal image acquisi-
tions, the prostate tended to have a longer size in AP and
SI direction compared to that in transverse image acqui-
sitions. When the distance from the probe surface to the
anterior prostate edge was compared between the two
types of image acquisitions, it tended to be longer in the
sagittal image acquisitions compared to that in the trans-
verse image acquisitions. In addition, the prostate volume
on the sagittal image acquisitions was significantly larger
than that on the transverse image acquisitions. Mean in-
ter-observer variation was 0.17 cm (SD = 0.10 cm). Figure 4
shows the relationships among the DVH parameters on
the post-implant CT analysis and the difference of the two
types of image acquisitions. Interestingly, relative size of
prostate apex in AP direction (No. 1 on Figure 1) in sag-
itual image acquisitions compared to transverse image ac-
quisions was related to pD90 and pV100 in post-implanted
CT analysis. There was no significant relationships among
other DVH parameters and patient’s characteristics.
Table 3 and Figure 5 show the result of a phantom study.
There was no apparent difference in the phantom size
among the two types of image acquisitions and CT im-
gages. Although about 2 mm differences in the LR and SI
directions were seen between ultrasonography (US) and
CT images, it was probably caused by low visibility of the
phantom edge in the CT images (Figure 5).

Discussion

Our phantom study confirmed that the difference
of image acquisitions caused no difference of phantom
size. Therefore, the differences in the prostate contours
between the two types of image acquisitions would be

Table 2. Comparison of prostate size between
transverse and sagittal image acquisitions

| Directions     | Transverse (cm) | Sagittal (cm) | p value |
|----------------|-----------------|---------------|---------|
| 1. AP apex     | 1.57 ± 0.22     | 1.66 ± 0.25   | 0.0346  |
| 2. AP mid-gland| 2.80 ± 0.33     | 2.94 ± 0.37   | 0.0000  |
| 3. AP base     | 1.52 ± 0.20     | 1.60 ± 0.26   | 0.1819  |
| 4. LR apex     | 1.86 ± 0.30     | 1.90 ± 0.32   | 0.4970  |
| 5. LR mid-gland| 4.50 ± 0.42     | 4.45 ± 0.45   | 0.3619  |
| 6. LR base     | 2.41 ± 0.30     | 2.35 ± 0.34   | 0.3565  |
| 7. SI          | 3.44 ± 0.35     | 3.62 ± 0.38   | 0.0010  |
| 8. AP edge apex| 2.77 ± 0.24     | 3.06 ± 0.25   | 0.0000  |
| 9. AP edge mid-gland| 3.34 ± 0.34     | 3.60 ± 0.33   | 0.0000  |
| 10. AP edge base| 2.79 ± 0.26    | 2.98 ± 0.41   | 0.0068  |
| Volume (ml)    | 26.58 ± 7.82    | 28.86 ± 8.19  | 0.0010  |

AP – anterior-posterior, LR – left-right, SI – superior-inferior
Index numbers of directions were corresponding to that on Figure 1
Table 3. Comparison of the phantom size on the two types of image acquisitions and computed tomography

| Directions | Transverse (cm) | Sagittal (cm) | CT (cm) |
|------------|----------------|--------------|---------|
| 2. AP      | 5.63           | 5.66         | 5.65    |
| 5. LR      | 4.60           | 4.56         | 4.30    |
| 7. SI      | 4.37           | 4.37         | 4.20    |
| Volume (ml)| 60.57          | 60.67        | 60.82   |

CT – computed tomography

Index numbers of directions were corresponding to that on Figure 1

caused by other factors. The prostate gland has some elasticity, and its shape is deformable. In TRUS image acquisitions, there is no doubt that probe insertion has the most significant effect on anatomical change. Several papers have reported anatomical and dosimetric changes due to probe insertion or rectal balloon insertion [7,8,9]. The rectum has a natural backward bend from the sigmoid colon to the anus. The curved portion is usually at the level of the prostate mid-gland or the apex; however, the probe insertion causes the rectum to straighten. Although the anus is tightly fixed by the pelvic floor muscles, the rectum is loosely fixed by the surrounding fat tissue. Therefore, the soft tissue of the prostate can be extended in the AP direction, as our study reveals.

However, prostate size in sagittal image acquisitions were not always larger than that in transverse image acquisitions. Our study suggests that patients with relatively smaller size of prostate apex in AP direction in sagittal image acquisitions compared to that in transverse image acquisitions, tended to have low $pD_{90}$ and $pV_{100}$ in post-implanted CT analysis. There was no clear explanation about this relationship in this study. One of possible explanations might be prostate rotation. Not only extension but also rotation could occurred during probe insertion, although no data was available in this study. We aim to conduct further study to quantify prostate rotation due to the TRUS probe. With regard to prostate volume, a report by Ali et al. also compared transverse and sagittal image acquisitions [10]. They reported that in a group of patients with a small prostate size, the prostate volume in the sagittal image acquisitions was larger than that in the transverse image acquisitions, although the opposite result was shown in the large (> 50 cc) prostate group. Since the patients in our study had relatively small prostates (≤ 45 cc), our results were compatible with those of the small prostate group in the above-mentioned study.

There were several limitations that should be considered. Firstly, some slices were inevitably missed when performing axial or sagittal ultrasound acquisitions. Therefore, 2 mm or more gaps were presented in some patients, although most of images were acquired in 1 mm slice thickness. These gaps did not cause any contraction of prostate contours because the missing slices were automatically interpolated. Therefore, we believe that effects induced by these gaps would be minor. Secondly, because the initial plan of this study was only to compare the two types of image acquisitions, number of patients was set for this purpose only. Therefore, suggested relationships between DVH parameters and difference of the two types of image was not based on sufficient statistical power, and could not be explained by available data. We are planning to investigate these issues in a further study.

Conclusions

Our study revealed that there were small but significant differences in the prostate contours between the transverse and the sagittal planning images. Furthermore, our study suggested that the differences between the two types of image acquisitions might correlated to dosimetric results on CT analysis.
Fig. 5. Images of the phantom on the 2 types of transrectal ultrasound (TRUS) image acquisitions and on computed tomography (CT). There was no apparent differences among the transverse image acquisition (A-C), sagittal image acquisition (D-F), and CT images (G-I) on transverse (A, D, G), sagittal (B, E, H), and coronal (C, F, I) planes.

Disclosure

Dr. Ishiyama reports other from Medicon Co., Ltd., other from Nihon Medi-Physics. Co., Ltd., during the conduct of the study.

References

1. Davis BJ, Horwitz EM, Lee WR et al. American Brachytherapy Society consensus guidelines for transrectal ultrasound-guided permanent prostate brachytherapy. Brachytherapy 2012; 11: 6-19.
2. Guinot JL, Ricos JV, Tortajada MI et al. Comparison of permanent (125)I seeds implants with two different techniques in 500 cases of prostate cancer. J Contemp Brachytherapy 2015; 7: 258-264.
3. http://www.jastro.or.jp/customer/guideline/2016/10/977bf02b89c8fbd591c47911d7a3e5c5d648.pdf.
4. Stock RG, Stone NN, Wesson MF et al. A modified technique allowing interactive ultrasound-guided three-dimensional transperineal prostate implantation. Int J Radiat Oncol Biol Phys 1995; 32: 219-225.
5. Zauls AJ, Ashenafi MS, Onicescu G et al. Comparison of intraoperatively built custom linked seeds versus loose seed gun applicator technique using real-time intraoperative planning for permanent prostate brachytherapy. *Int J Radiat Oncol Biol Phys* 2011; 81: 1010-1016.

6. Ishiyama H, Satoh T, Kawakami S et al. A prospective quasi-randomized comparison of intraoperatively built custom-linked seeds versus loose seeds for prostate brachytherapy. *Int J Radiat Oncol Biol Phys* 2014; 90: 134-139.

7. Ishiyama H, Kitano M, Satoh T et al. Difference in rectal dosimetry between pre-plan and post-implant analysis in transperineal interstitial brachytherapy for prostate cancer. *Radiother Oncol* 2006; 78: 194-198.

8. Seppenwoolde Y, Kolkman-Deurloo IK, Sipkema D et al. HDR prostate monotherapy: dosimetric effects of implant deformation due to posture change between TRUS- and CT-imaging. *Radiother Oncol* 2008; 86: 114-119.

9. Otón LF, Dolado MC, Núñez EJ et al. Effect of constipation on dosimetry after permanent seed brachytherapy for prostate cancer. *J Contemp Brachytherapy* 2015; 5: 247-251.

10. Ali I, Algan O, Thompson S et al. A comparative study of seed localization and dose calculation on pre- and post-implantation ultrasound and CT images for low-dose-rate prostate brachytherapy. *Phys Med Biol* 2009; 54: 5595-5611.