Mathematical modeling in full-field optical coherence elastography∗

Habib Ammari† Elie Bretin‡ Pierre Millien† Laurent Seppecher†
Jin-Keun Seo§

May 21, 2014

Abstract

We provide a mathematical analysis of and a numerical framework for full-field optical coherence elastography, which has unique features including micron-scale resolution, real-time processing, and non-invasive imaging. We develop a novel algorithm for transforming volumetric optical images before and after the mechanical solicitation of a sample with sub-cellular resolution into quantitative shear modulus distributions. This has the potential to improve sensitivities and specificities in the biological and clinical applications of optical coherence tomography.

Mathematics Subject Classification (MSC2000): 35R30, 35B30.

Keywords: full-field optical coherence tomography, elastography, hybrid imaging, optimal control, high-resolution shear modulus imaging, biological tissues.

1 Introduction

Optical coherence tomography (OCT) is a non-invasive and a non-ionizing imaging technique that produces high-resolution images of biological tissues. It performs optical slicing in the sample, to allow three-dimensional reconstructions of internal structures. Conventional optical coherence time-domain and frequency-domain tomographies require transverse scanning of the illumination spot in one or two directions to obtain cross-sectional or en face images, respectively. Full-field OCT allows OCT to be performed without transverse scanning; the tomographic images are obtained by combining interferometric images acquired in parallel using an image sensor. Both the transverse and the axial resolutions are of the order of 1μm; see [9, 10]. We refer to [11] for the mathematical modeling of OCT.

∗This work was supported by the ERC Advanced Grant Project MULTIMOD–267184.
†Department of Mathematics and Applications, Ecole Normale Supérieure, 45 Rue d’Ulm, 75005 Paris, France (habib.ammari@ens.fr, pierre.millien@ens.fr, laurent.seppecher@ens.fr).
‡Institut Camille Jordan, Université de Lyon, Lyon, F-69003, France (bretin@cmap.polytechnique.fr).
§Department of Computational Science and Engineering, Yonsei University, 50 Yonsei-Ro, Seodaemun-Gu, Seoul 120-749, Korea (seoj@yonsei.ac.kr).
Elastography is an imaging-based technique for the estimation of the elastic properties of tissues. Given that the mechanical properties of tissues and cells are related to their structure and function, changes in those properties can reflect healthy or pathological states such as weakening of vessel walls or cirrhosis of the liver. Elastography can aid the identification of suspicious lesions, the diagnosis of various diseases and the monitoring of the effectiveness of treatments (see [15, 16]). Different imaging modalities (e.g., ultrasound and magnetic resonance imaging) can be used to measure tissue displacements and to estimate the resulting tissue stiffness and viscosity. Magnetic resonance elastography is relatively expensive, due to the high magnetic field environment, which requires specifically designed equipment. Several reconstruction approaches for elastography have been derived [3, 4, 5, 22].

In [18], elastographic contrast has been combined with full-field OCT with the aim of creating a virtual palpation map at the micrometer scale. The idea is to register a volumetric optical image before and after mechanical solicitation of the sample. Based on the assumption that the density of the optical scatterers is advected by the deformation, the displacement map can be first estimated. Then, using a quasi-incompressible model for the tissue elasticity, the shear modulus distribution can be reconstructed from the estimated displacement map.

The OCT elastography is able to perform displacement measurements with sub-cellular resolution. It enables a more precise characterization of tissues than that achieved using ultrasound or magnetic resonance elastography; therefore, it provides a more accurate assessment of microscale variations of elastic properties. A map of mechanical properties added as a supplementary contrast mechanism to morphological images could aid diagnosis. The technique costs less than other elastography techniques.

The mapping of mechanical properties was first introduced to OCT imaging by Schmitt [21], who measured displacements as small as a few micrometers in heterogeneous gelatin phantoms containing scattering particles in addition to living skin. Various subsequent applications have employed OCT methods in elastography; these include dynamic and full-field optical coherence elastography (see [14, 19, 20]).

In all of the aforementioned techniques, transforming the OCT images before and after the application of a load into quantitative maps of the shear modulus is a challenging problem.

In this paper we present a mathematical and numerical framework for the OCT-elastography experiment described in [18]. Using the set of images before and after mechanical solicitation we design a novel method to reconstruct the shear modulus distribution inside the sample.

To mathematically formulate the problem, let $\Omega_0 \subset \mathbb{R}^d, d = 2, 3$, and let $\varepsilon_0$ be the known piecewise smooth optical index of the medium, and $\mu$ be its shear modulus. In this paper we consider heterogeneous (unknown) shear modulus distributions. The medium is solicited mechanically. Since compression modulus of biological media is four order of magnitude larger than the shear modulus, it can be shown that the displacement map $u$ obeys the linearized equations of incompressible fluids or the Stokes system [3, 4, 5]. The model problem is then the following Stokes system in a heterogeneous medium which reads:

\[
\begin{align*}
\nabla \cdot (\mu(\nabla u + \nabla u^T)) + \nabla p &= 0 \quad \text{in} \quad \Omega_0, \\
\n\nabla \cdot u &= 0 \quad \text{in} \quad \Omega_0, \\
\n\nabla \cdot u &= 0 \quad \text{on} \quad \partial \Omega_0, \\
\n\n\nabla \cdot u &= f \quad \text{on} \quad \partial \Omega_0, \\
\end{align*}
\] (1.1)
where superposed $T$ denotes the transpose and the real-valued vector $\mathbf{f}$ satisfies the compatibility condition $\int_{\partial \Omega_0} \mathbf{f} \cdot \mathbf{\nu} = 0$ with $\mathbf{\nu}$ being the outward normal at $\partial \Omega_0$.

Throughout this paper, we assume that $\mu \in C^{0,1}(\overline{\Omega}_0)$ and $\mathbf{f} \in C^2(\partial \Omega_0)^d$. From [7, 12, 13], (1.1) has a unique solution $\mathbf{u} \in C^1(\overline{\Omega}_0)^d$. Moreover, there exists a positive constant $C$ depending only on $\mu$ and $\Omega_0$ such that

\[ ||\mathbf{u}||_{C^1(\overline{\Omega}_0)^d} \leq C||\mathbf{f}||_{C^2(\partial \Omega_0)^d}. \]

Using a second OCT scan, one has access to the optical index of the deformed medium $\varepsilon_u(\tilde{x})$, $\forall \tilde{x} \in \Omega_u$, where $\Omega_u$ is defined by

\[ \Omega_u = \{ \mathbf{x} + \mathbf{u}(\mathbf{x}), \mathbf{x} \in \Omega_0 \}. \]

The new optical index is linked to the original one by

\[ \varepsilon(\mathbf{x}) = \varepsilon_u(\mathbf{x} + \mathbf{u}(\mathbf{x})), \quad \forall \mathbf{x} \in \Omega_0. \tag{1.2} \]

The goal is to reconstruct the shear modulus map $\mu$ on $\Omega_0$ from the functions $\varepsilon$ and $\varepsilon_u$. We first prove that, in two dimensions, if the direction of $\nabla \varepsilon / ||\nabla \varepsilon||$ is not constant in a neighborhood of $\mathbf{x}$, then the displacement field $\mathbf{u}$ at $\mathbf{x}$ can be approximately reconstructed. In three dimensions, one shall assume that the vectors $\nabla \varepsilon(\mathbf{y}) / ||\nabla \varepsilon(\mathbf{y})||$ are not coplanar for $\mathbf{y}$ a neighborhood of $\mathbf{x}$. Hence, the reconstructed value of $\mathbf{u}(\mathbf{x})$ serves as an initial guess for the minimization of the discrepancy between computed and measured changes in the optical index. Then, we compute an element of the subgradient $\delta$ of the discrepancy functional. Finally, we implement a minimization scheme to retrieve the shear modulus map from the reconstructed displacements.

The paper is organized as follows. Section 2 is devoted to some mathematical preliminaries. In section 3 we consider piecewise smooth $\varepsilon$ functions and first derive a leading-order Taylor expansion of $\varepsilon_u$ as $||\mathbf{u}||_{C^1}$ goes to zero. Then we provide an initial guess by linearization. Finally, we prove the Fréchet differentiability of the discrepancy functional between the measured and the computed advected images. The displacement field inside the sample can be obtained as the minimizer of such functional. Section 4 is devoted to the reconstruction of the shear modulus from the displacement measurements. In section 5 we present some numerical results to highlight the viability and the performance of the proposed algorithm. The paper ends with a short discussion.

2 Preliminaries

Let $\Omega$ be a bounded smooth domain in $\mathbb{R}^d$, $d = 2, 3$. We start by defining a class of piecewise smooth functions.

**Definition 2.1** For any $k \in \mathbb{N}$, $\alpha \in [0, 1]$, for any curve $S$ of class $C^{1,\alpha}$ for some $0 < \alpha < 1$ such that $\Omega \setminus S$ is a union of connected domains $\Omega_i$, $i = 1, 2, \cdots n$, we define $C^{k,\alpha}_S(\overline{\Omega})$ to be the class of functions $f : \Omega \rightarrow \mathbb{R}$ satisfying

\[ f|_{\Omega_i} \in C^{k,\alpha}_S(\overline{\Omega_i}) \quad \forall i = 1, \cdots n. \tag{2.1} \]
Definition 2.2 We define $\text{BV}(\Omega)$ as the subspace of $L^1(\Omega)$ of all the functions $f$ whose weak derivative $Df$ is a finite Radon measure. In other terms, $f$ satisfies

$$\int_\Omega f \nabla \cdot F \leq C \sup_{x \in \Omega} |F|, \quad \forall F \in C^1_0(\Omega)^d$$

for some positive constant $C$ with $C^1_0(\Omega)$ being the set of compactly supported $C^1$ functions.

The derivative of a function $f \in \text{BV}(\Omega)$ can be decomposed as

$$Df = \nabla f \mathcal{H}^d + [f] \nu_s \mathcal{H}_S^{d-1} + D_c f,$$

where $\mathcal{H}^d$ is the Lebesgue measure on $\Omega$, $\mathcal{H}_S^{d-1}$ is the surface Hausdorff measure on a rectifiable surface $S$, $\nu_S$ is a normal vector defined a.e. on $S$, $\nabla f \in L^1(\Omega)$ is the smooth derivative of $f$, $[f] \in L^1(S, \mathcal{H}_S^{d-1})$ is the jump of $f$ across $S$ and $D_c f$ is a vector measure supported on a set of Hausdorff dimension less than $(d-1)$, which means that its $(d-1)$-Hausdorff-measure is zero; see [1].

Definition 2.3 We define $\text{SBV}(\Omega)$ as the subspace of $\text{BV}(\Omega)$ of all the functions $f$ satisfying $D_c f = 0$.

Definition 2.4 For any $1 \leq p \leq +\infty$, we define

$$\text{SBV}^p(\Omega) = \{ f \in \text{SBV}(\Omega) \cap L^p(\Omega), \ \nabla f \in L^p(\Omega)^d \}.$$

As $\text{SBV}(\Omega)$ is a good model for piecewise-$W^{1,1}$ functions, the space $\text{SBV}^p(\Omega)$ can be seen as the space of piecewise-$W^{1,p}$ functions. Here, $W^{1,p}(\Omega) = \{ f \in L^p(\Omega), \ \nabla f \in L^p(\Omega)^d \}$ for $p \geq 1$.

Note that the space $\text{SBV}^\infty(\Omega)$ is a nice definition of piecewise Lipschitz function. Note also that $C^{k,\alpha}_S(\Omega) \subset \text{SBV}^p(\Omega)$.

From now on, we assume that the optical index in the medium $\varepsilon$ belongs to $C^{k,\alpha}_S(\overline{\Omega})$, which is a simple but good model for a discontinuous medium. Some of the following propositions are true for more general maps $\varepsilon \in \text{SBV}(\Omega)$. In these propositions we only assume that $\varepsilon$ is in $\text{SBV}(\Omega)$.

3 Displacement field measurements

3.1 First order approximation

Let $\Omega \Subset (\Omega_0 \cap \Omega_u)$ be a smooth simply connected domain. On $\Omega$, we have

$$\varepsilon_u = \varepsilon \circ (I + \mathbf{u})^{-1},$$

$$\varepsilon = \varepsilon_u \circ (I + \mathbf{u}),$$

where $I$ is the $d \times d$ identity matrix.

Proposition 3.1 Let $\varepsilon \in \text{BV}(\Omega)$ and let $\mathbf{u} \in C^1(\overline{\Omega})^d$ be such that $\|\mathbf{u}\|_{C^1(\overline{\Omega})^d} < 1$. Then, for any $\psi \in C^0_0(\Omega)$, we have

$$\left| \int_\Omega (\varepsilon - \varepsilon_u) \psi - \int_\Omega \psi \mathbf{u} \cdot D\varepsilon \right| \leq C \|\mathbf{u}\|_{C^0(\overline{\Omega})^d} \|\mathbf{u}\|_{C^1(\overline{\Omega})^d} \|\psi\|_{C^0_0(\Omega)} \|\varepsilon\|_{\text{TV}(\Omega)}, \quad (3.1)$$
where the constant $C$ is independent of $\psi$ and $|\cdot|_{TV(\Omega)}$ denotes the total variation seminorm. Estimate (3.1) yields that 
\[ \frac{\varepsilon_u - \varepsilon + u \cdot D\varepsilon}{\|u\|_{C^0(\Omega)^d}} \text{ weakly converges to } 0 \text{ in } C^1_0(\Omega) \text{ when } \|u\|_{C^1(\Omega)^d} \text{ goes to } 0. \]

**Proof.** For each $t \in [0, 1]$, define $\phi_t(x)$ by $\phi_t^{-1}(x) = x + tu(x)$. Let $\eta > 0$ be a small parameter, and $\varepsilon^{(n)}$ be a smooth function such that $\|\varepsilon - \varepsilon^{(n)}\|_{L^1(\Omega)} \to 0$, and $|\varepsilon^{(n)}|_{TV(\Omega)} \to |\varepsilon|_{TV(\Omega)}$ as $\eta \to 0$. Analogously, we define $\varepsilon^{(n)}_u$ to be the smooth approximation of $\varepsilon_u$ given by 
\[ \varepsilon^{(n)}_u(x) = \varepsilon^{(n)} \circ \phi_1(x). \]
From 
\[ \varepsilon^{(n)}_u(x) - \varepsilon^{(n)}(x) = (\varepsilon^{(n)} \circ \phi_1)(x) - (\varepsilon^{(n)} \circ \phi_0)(x), \quad \forall x \in \Omega, \]
we have 
\[ \varepsilon^{(n)}_u(x) - \varepsilon^{(n)}(x) = \int_0^1 \nabla \varepsilon^{(n)}(\phi_t(x)) \cdot \partial_t \phi_t(x) dt, \quad \forall x \in \Omega. \]
Therefore, for $\psi \in C^\infty_0(\Omega)$ with $C^\infty_0(\Omega)$ being the set of compactly supported $C^\infty$ functions, 
\[ \int_\Omega \left[ \varepsilon^{(n)}_u(x) - \varepsilon^{(n)}(x) + \nabla \varepsilon^{(n)}(x) \cdot u(x) \right] \psi(x) dx = \]
\[ \int_\Omega \left[ \int_0^1 \nabla \varepsilon^{(n)}(\phi_t(x)) \cdot \partial_t \phi_t(x) dt \right] \psi(x) dx + \int_\Omega \nabla \varepsilon^{(n)}(x) \cdot u(x) \psi(x) dx, \quad \forall x \in \Omega. \quad (3.2) \]
By a change of variables in the first integral and using the fact that 
\[ \partial_t \phi_t(x) = -\partial_x \phi_t(x) \partial_t \phi_t^{-1}(y) |_{y = \phi_t(x)}, \]
we get, for all $x \in \Omega,$ 
\[ \int_0^1 \left[ \int_\Omega \nabla \varepsilon^{(n)}(\phi_t(x)) \cdot \partial_t \phi_t(x) \psi(x) dx \right] dt = \]
\[ -\int_0^1 \int_\Omega \nabla \varepsilon^{(n)}(y) \cdot \left[ \partial_x \phi_t(\phi_t^{-1}(y)) \partial_t \phi_t^{-1}(y) \right] |\det \partial_x \phi_t^{-1}(y)| \psi(\phi_t^{-1}(y)) dy dt. \]
Here, $\det$ denotes the determinant of a matrix. Since 
\[ \forall (y, t) \in \Omega \times [0, 1], \quad \partial_t \phi_t^{-1}(y) = u(y), \]
\[ \partial_y \phi_t^{-1}(y) = \mathbb{I} + t \nabla u(y), \]
and 
\[ \partial_x \phi_t(\phi_t^{-1}(y)) \partial_y \phi_t^{-1}(y) = \mathbb{I}, \]
we can write 
\[ \int_0^1 \int_\Omega \left[ \nabla \varepsilon^{(n)}(\phi_t(x)) \cdot \partial_t \phi_t(x) \psi(x) dx \right] dt = \]
\[ -\int_0^1 \int_\Omega \nabla \varepsilon^{(n)}(y) \cdot \left[ (\mathbb{I} + t \nabla u(y))^{-1} u(y) \right] |\det \mathbb{I} + t \nabla u(y)| \psi(\phi_t^{-1}(y)) dy dt, \]
\[ 5 \]
and hence,

\[
\int_{\Omega} \left[ \varepsilon^{(n)}_u(x) - \varepsilon^{(n)}(x) + \nabla \varepsilon^{(n)}(x) \cdot u(x) \right] \psi(x) dx = \\
\int_0^1 \int_{\Omega} \nabla \varepsilon^{(n)}(x) \cdot u(x) \left[ \psi(x) - \psi \left( \phi_t^{-1}(x) \right) \right] dx dt \\
+ \int_0^1 \int_{\Omega} \nabla \varepsilon^{(n)}(x) \cdot \left( (I + t \nabla u(x))^{-1} \right| \det I + t \nabla u(x) \left| - I \right| u(x) \psi \left( \phi_t^{-1}(x) \right) dx dt.
\]

The first term in the right-hand side of (3.3) can be estimated as follows:

\[
\left| \int_0^1 \int_{\Omega} \nabla \varepsilon^{(n)}(x) \cdot u(x) \left[ \psi(x) - \psi \left( \phi_t^{-1}(x) \right) \right] dx dt \right| \leq \| u \|^2_{C^0(\Omega)^d} \| \nabla \varepsilon^{(n)} \|^2_{L^1(\Omega)^d} \| \nabla \psi \|^2_{C^0(\Omega)^d}.
\]

Let \( \text{tr} \) denote the trace of a matrix. Using the fact that

\[
(I + t \nabla u)^{-1} = \sum_{i=0}^{d-1} \frac{(-1)^i}{(t \nabla u)^i},
\]

which follows from \( \| u \|_{C^1(\Omega)^d} < 1 \), and

\[
\det (I + t \nabla u) = \begin{cases} 
1 - \text{tr} t \nabla u + \text{det} t \nabla u & \text{if } d = 2, \\
1 + \text{tr} t \nabla u - \frac{1}{2} \left[ (\text{tr} t \nabla u)^2 - \text{det} (t \nabla u)^2 \right] + \text{det} t \nabla u & \text{if } d = 3,
\end{cases}
\]

we get

\[
\int_0^1 \int_{\Omega} \nabla \varepsilon^{(n)}(x) \cdot u(x) \left[ (I + t \nabla u(x))^{-1} \right| \det I + t \nabla u(x) \left| - I \right| \psi \left( \phi_t^{-1}(x) \right) dx dt \\
\leq \| u \|^2_{C^0(\Omega)^d} \| u \|^2_{C^1(\Omega)^d} \| \nabla \varepsilon^{(n)} \|^2_{L^2(\Omega)^d} \| \psi \|^2_{C^0(\Omega)^d},
\]

which is the desired estimate for the second term in the right-hand side of (3.3).

Now, we can deduce the final result by density when \( \eta \to 0 \). Since \( u \in C^1(\Omega)^d \) and \( \psi \in C_0^1(\Omega) \), we can write

\[
\int_{\Omega} \psi u \cdot \nabla \varepsilon^{(n)} = - \int_{\Omega} \nabla \cdot (\psi u) \varepsilon^{(n)}.
\]

Since \( \| \varepsilon^{(n)} \|_{L^1(\Omega)} \to 0 \), we have

\[
\int_{\Omega} \nabla \cdot (\psi u) \varepsilon^{(n)} \to \int_{\Omega} \nabla \cdot (\psi u) \varepsilon.
\]

As \( \| \varepsilon \|_{TV(\Omega)} \to \| \varepsilon \|_{TV(\Omega)} \), we arrive at (3.1) and the proof of the proposition is complete. □
3.2 Local recovery via linearization

Assuming that $\varepsilon \in SBV^2(\Omega)$, we can write

$$D\varepsilon = \nabla \varepsilon \mathcal{H}^d + [\varepsilon]_{\mathcal{S}} \nu_S \mathcal{H}^{d-1}_S,$$

where $\nu_S$ is the outward normal at the oriented surface $S$ of discontinuity of $\varepsilon$.

The data consists of $\varepsilon$ and $\varepsilon_u$ on $\Omega$. In order to reconstruct $u$, we can use the first order approximation of $\varepsilon - \varepsilon_u$:

$$\varepsilon - \varepsilon_u \approx u \cdot D\varepsilon,$$

given by Proposition 3.1. These data can be decomposed into two parts:

$$u \cdot D\varepsilon(\cdot) = u \cdot \nabla \varepsilon \mathcal{H}^d + [\varepsilon]_{\mathcal{S}} u \cdot \nu_S \mathcal{H}^{d-1}_S = d_{\text{reg}} \mathcal{H}^d + d_{\text{sing}} \mathcal{H}^{d-1}_S.$$

Let $w$ be a mollifier supported on $[-1, 1]$. For any $\delta > 0$, we define

$$w_\delta = \frac{1}{\delta^d} w \left( \frac{\cdot}{\delta} \right),$$

and introduce

$$u_\delta(x) = \int_{\Omega} u(y) w_\delta(|x - y|) dy.$$ 

Since $u$ is smooth, for any $x \in \Omega$, $u_\delta(x)$ is a good approximation of $u$ on the ball with center $x$ and radius $\delta$.

We want to find an approximate value for $u_\delta$ from the optical measurements and use it as an initial guess in an optimization procedure. For doing so, we introduce the functional $J_x : \mathbb{R}^d \rightarrow \mathbb{R}$ given by

$$u \mapsto J_x(u) = \int_{\Omega} |\nabla \varepsilon(y) \cdot u - d_{\text{reg}}(y)|^2 w_\delta(|x - y|) dy$$

$$+ \int_{\Omega} |[\varepsilon]_{\mathcal{S}} u \cdot \nu_S - d_{\text{sing}}(y)|^2 w_\delta(|x - y|) dy,$$

and look for minimizers of $J_x$ in $\mathbb{R}^d$. The gradient of $J_x$ can be explicitly computed as follows:

$$\nabla J_x(u) = 2 \int_{\Omega} (\nabla \varepsilon(y) \cdot u - d_{\text{reg}}(y)) \nabla \varepsilon(y) w_\delta(|x - y|) dy$$

$$+ 2 \int_{\Omega} ([\varepsilon]_{\mathcal{S}} u \cdot \nu_S(y) - d_{\text{sing}}(y)) [\varepsilon]_{\mathcal{S}} \nu_S(y) w_\delta(|x - y|) dy.$$ 

In the case where $\varepsilon$ has no jumps, $J_x$ is a quadratic functional and we have

$$\nabla J_x(u) = 0 \iff u^T \left( \int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \right) = \int_{x+\delta B} d_{\text{reg}}(y) w_\delta(|x - y|) \nabla \varepsilon(y) dy,$$

where $B$ is the ball with center $0$ and radius $1$.

If the matrix $\int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy$ is invertible, then the minimizer is given by

$$u^T = \left( \int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \right)^{-1} \int_{x+\delta B} d_{\text{reg}} w_\delta(|x - y|) \nabla \varepsilon(y) dy.$$ (3.5)
The following proposition gives a sufficient condition for the invertibility of the matrix 
\[ \int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \]  

**Proposition 3.2** Suppose that \( \varepsilon \) has no jumps and \( d = 2 \). Assume \( x + \delta B \subset \Omega \). Then, if all vectors \( \nabla \varepsilon \) in \( \{ y : w_\delta(|y - x|) \neq 0 \} \) are not collinear, then the matrix 
\[ \int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \]

is invertible.

**Proof.** Writing 
\[ \forall y \in x + \delta B, \quad \nabla \varepsilon(y) = u(y)e_1 + v(y)e_2, \]
where \( \{e_1, e_2\} \) is the canonical basis of \( \mathbb{R}^2 \), it follows that 
\[ \nabla \varepsilon \nabla \varepsilon^T = u^2(y)e_1e_1^T + v^2(y)e_2e_2^T + u(y)v(y)(e_1e_2^T + e_2e_1^T), \quad \forall y \in x + \delta B. \]
Computing the convolution with respect to \( w_\delta \), we get 
\[ \int_{\Omega} w_\delta(|y - x|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy = \left( \int_{\Omega} u^2(y)w_\delta(|y - x|)dy \right) e_1e_1^T + \left( \int_{\Omega} v^2(y)w_\delta(|y - x|)dy \right) e_2e_2^T + \left( \int_{\Omega} u(y)v(y)w_\delta^2(|y - x|)dy \right) (e_1e_2^T + e_2e_1^T). \]
This matrix is not invertible if and only if 
\[ \left( \int_{\Omega} u^2(y)w_\delta(|y - x|)dy \right) \left( \int_{\Omega} v^2(y)w_\delta(|y - x|)dy \right) = \left( \int_{\Omega} u(y)v(y)w_\delta(|y - x|)dy \right)^2, \]
which is exactly the equality case in weighted Cauchy-Schwarz inequality. So, if there exist two points \( y_1, y_2 \in \{ y : w_\delta(|y - x|) \neq 0 \} \) such that \( \nabla \varepsilon(y_1) \times \nabla \varepsilon(y_2) \neq 0 \), then \( u \) is not proportional to \( v \), and the matrix is invertible. \( \square \)

**Remark 3.3** Assuming that \( \nabla \varepsilon(y) \neq 0 \) for \( y \in x + \delta B \subset \Omega \), Proposition 3.2 gives that the direction of \( \frac{\nabla \varepsilon}{|\nabla \varepsilon|} \) is not constant in \( x + \delta B \subset \Omega \) if and only if 
\[ \int_{x + \delta B} \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \]

is invertible. Hence, under the above condition on \( \varepsilon \) in the neighborhood \( x + \delta B \), the displacement field \( u \) at \( x \) can be approximately reconstructed.

**Remark 3.4** By exactly the same arguments as those in two dimensions, one can prove that in the three-dimensional case, if all vectors \( \nabla \varepsilon \) in \( \{ y : w_\delta(|y - x|) \neq 0 \} \) are not coplanar, then the matrix 
\[ \int_{\Omega} w_\delta(|x - y|) \nabla \varepsilon(y) \nabla \varepsilon^T(y) dy \]
is invertible.

On the other hand, in the case where \( \varepsilon \) is piecewise smooth, one can first detect the surface of jumps of \( \varepsilon \) using for example an edge detection algorithm \([6, 17]\) and then apply the proposed local algorithm in order to have a good approximation of \( u \) in the domains where \( \varepsilon \) is smooth.
3.3 Minimization of the discrepancy functional

Let \( \varepsilon \in C^{k,\alpha}_S (\Omega) \), where \( S \) is the surface of discontinuity. For the sake of simplicity we assume that \( \Omega \setminus S \) is the union of two connected domains \( \Omega_1 \cup \Omega_2 \). Therefore, \( \varepsilon \) can be written as
\[
\varepsilon = \varepsilon_1 \chi_{\Omega_1} + \varepsilon_2 \chi_{\Omega_2}
\]
with \( \varepsilon_i \in C^1(\Omega_i) \), for \( i = 1, 2 \).

Denote \( u^* \) the applied (true) displacement on \( \Omega \) (as defined in (1.1)) and \( \tilde{\varepsilon} \) the measured deformed optical index given by
\[
\tilde{\varepsilon} = \varepsilon \circ (I + u^*)^{-1}.
\]

The following result holds.

**Proposition 3.5** Let \( \varepsilon \) verify (3.6), \( u^* \in C^1(\Omega)^d \) be the solution of (1.1), and \( \tilde{\varepsilon} = \varepsilon \circ (I + u^*)^{-1} \). Suppose that \( \Omega_2 \subseteq \Omega \). Then, the functional \( I \) defined by
\[
I : C^1(\Omega)^d \longrightarrow \mathbb{R},
\]
\[
u \mapsto I(u) = \int_{\Omega} |\tilde{\varepsilon} \circ (I + u) - \varepsilon|^2 \, dx
\]
has a nonempty subgradient. Let \( \xi \) in the dual of \( C^1(\Omega)^d \) be given by
\[
\xi : h \mapsto 2 \int_{\Omega} [\tilde{\varepsilon}(x + u) - \varepsilon(x)] h(x) \cdot D \tilde{\varepsilon} \circ (I + u)(x) \, dx.
\]

For \( ||h||_{C^1(\Omega)^d} \) small enough, we have
\[
I(u + h) - I(u) \geq (\xi, h),
\]
where \( (\cdot, \cdot) \) is the duality product between \( C^1(\Omega)^d \) and its dual, which means that \( \xi \in \partial I \) with \( \partial I \) being the subgradient of \( I \).

**Remark 3.6** It is worth emphasizing that if \( \varepsilon \) has no jump, then \( I \) is Fréchet differentiable and \( \xi \) is its Fréchet derivative.

**Remark 3.7** Under the assumptions of Proposition 3.5, if \( u^* \) is small enough (in \( C^1 \)-norm), then \( \tilde{\varepsilon} = \varepsilon \circ (I + u^*)^{-1} \) can be written as
\[
\tilde{\varepsilon} = \tilde{\varepsilon}_1 + \tilde{\varepsilon}_2 \chi_{\Omega_2},
\]
with \( \tilde{\varepsilon}_1 \in C^1(\Omega) \) and \( \tilde{\varepsilon}_2 \in C^1_0(\Omega) \). In the sequel, we shall define \( \tilde{\Omega}_i = (I + u^*) (\Omega_i) \) and \( \tilde{f}_i = \varepsilon_i \circ (I + u^*)^{-1} \). For doing so, we extend \( \tilde{f}_i \) into a function \( \tilde{\varepsilon}_1 \) defined on the whole domain such that \( \tilde{\varepsilon}_1 \in C^1(\Omega) \) and \( \tilde{\varepsilon}_1|\Omega_1 = \tilde{f}_1 \). Then, we set \( \tilde{\varepsilon}_2 = \tilde{f}_2 - \tilde{\varepsilon}_1 \) on \( \tilde{\Omega}_2 \). Finally, we extend \( \tilde{\varepsilon}_2 \) into a compactly supported \( C^1 \)-function on the whole domain \( \Omega \).

We first prove the following lemma.
Lemma 3.8 Let \( u, h \in C^1(\Omega)^d \) and let \( \tilde{e} \) be as in (3.9). Then, for \( \|u - u^*\|_{C^1(\Omega)^d} \) and \( \|h\|_{C^1(\Omega)^d} \) small enough, we have

\[
\int_{\Omega} [\tilde{e}(x + u + h) - \tilde{e}(x + u)]^2 \, dx = \int_{\Omega} \tilde{e}_2^2(x+u) |h \cdot \nu| \delta_{\Omega_2}(x+u) \, dx + o(\|h\|_{C^1(\Omega)^d}), \tag{3.10}
\]

where \( \delta_{\partial \Omega_2} \) is the Dirac distribution on \( \partial \Omega_2 \) and \( \tilde{e}_2 \) is defined in Remark 3.7.

Proof. We start by decomposing \( \tilde{e} \) as follows:

\[
\int_{\Omega} [\tilde{e}(x + u + h) - \tilde{e}(x + u)]^2 \, dx = \int_{\Omega} \left( \tilde{e}_1(x+u+h) - \tilde{e}_1(x+u) \right) + \left( \tilde{e}_2(x+u+h) - \tilde{e}_2(x+u) \right) \, dx.
\]

Now, by developing the square, the first term can be estimated by

\[
\left| \int_{\Omega} \left( \tilde{e}_1(x+u+h) - \tilde{e}_1(x+u) \right)^2 \, dx \right| \leq \|\tilde{e}_1\|_{C^1(\Omega)}^2 \|h\|_{C^1(\Omega)^d}^2.
\]

Next, we write

\[
\tilde{e}_2(x+u+h) - \tilde{e}_2(x+u) = \left[ \tilde{e}_2(x+u+h) - \tilde{e}_2(x+u) \right] \chi_{\Omega_2}(x+u+h) + \left[ \tilde{e}_2(x+u+h) - \tilde{e}_2(x+u) \right] \tilde{e}_2(x+u).
\]

Since \( \tilde{e}_1(x+u+h) - \tilde{e}_1(x+u) \tilde{e}_2(x+u) \in C_0^1(\Omega) \), Proposition 3.1 yields

\[
\leq C \left( \int_{\Omega} |h \cdot \nabla \tilde{e}_1(x+u)|^2 \, dx \right)^{1/2} \left( \int_{\Omega} |h \cdot \nu \tilde{e}_2(x+u)|^2 \delta_{\partial \Omega_2}(x+u) \, dx \right) + o(\|h\|_{C^1(\Omega)^d})^{1/2}
\]

\[
\leq C\|h\|_{C^1(\Omega)^d}^2.
\]

We now need to handle the last term

\[
\int_{\Omega} \left[ \chi_{\Omega_2}(x+u+h) - \chi_{\Omega_2}(x+u) \right] \tilde{e}_2(x+u) \, dx = \int_{\Omega} \chi_{\Omega_2}(x+u+h) - \chi_{\Omega_2}(x+u) \tilde{e}_2(x+u) \, dx.
\]

Using Proposition 3.1, we obtain that

\[
\int_{\Omega} \left[ \chi_{\Omega_2}(x+u+h) - \chi_{\Omega_2}(x+u) \right] \tilde{e}_2(x+u) \, dx = \int_{\Omega} \tilde{e}_2^2(x+u) |h \cdot \nu| \delta_{\partial \Omega_2}(x+u) \, dx + o(\|h\|_{C^1(\Omega)^d}),
\]

which completes the proof of the lemma. \(\square\)

We are now ready to prove Proposition 3.5.
Proof. If \( u \in C^1(\Omega)^d \) and \( h \in C^1(\Omega)^2 \), then we have

\[
I(u + h) - I(u) = \int_{\Omega} [\bar{\varepsilon}(x + u + h) + \varepsilon(x + u) - 2\varepsilon(x)] \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx,
\]
and hence,

\[
I(u + h) - I(u) = \int_{\Omega} [\bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u)]^2 \, dx + 2 \int_{\Omega} [\bar{\varepsilon}(x + u) - \varepsilon(x)] \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx.
\]

For any \( \eta > 0 \), let \( g^{(\eta)} \) be a smooth, compactly supported function such that

\[
\|g^{(\eta)} - [\bar{\varepsilon} \circ (I + u) - \varepsilon]\|_{L^2(\Omega)} < \eta \quad \text{and} \quad \|g^{(\eta)}|_{TV(\Omega)} - |\bar{\varepsilon} \circ (I + u) - \varepsilon|_{TV(\Omega)} < \eta;
\]
see [2].

Now, we write

\[
\int_{\Omega} [\bar{\varepsilon}(x + u) - \varepsilon(x)] \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx = \int_{\Omega} g^{(\eta)}(x) \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx
\]

\[
+ \int_{\Omega} [\bar{\varepsilon}(x + u) - \varepsilon(x) - g^{(\eta)}(x)] \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx.
\]

Let \( \tau_h \) be the translation operator. Then, \( \tau_h \) satisfies, for any \( h \in C^1(\Omega)^d \),

\[
\|\tau_h[f] - f\|_p \leq C(\eta)\|h\|_{C^1(\Omega)^d}, \quad \forall f \in SBV^p(\Omega).
\]

Using Cauchy-Schwartz’ inequality, we get

\[
\left| \int_{\Omega} [\bar{\varepsilon}(x + u) - \varepsilon(x) - g^{(\eta)}(x)] \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx \right| \leq C\eta\|h\|_{C^1(\Omega)^d},
\]

where \( C \) is a constant depending on \( \bar{\varepsilon}, u, \) and \( \Omega \).

We know that for a certain function \( \rho \) such that \( \rho(s) \to 0 \) when \( s \to 0 \):

\[
\left| \int_{\Omega} g^{(\eta)}(x) \left[ \bar{\varepsilon}(x + u + h) - \bar{\varepsilon}(x + u) \right] \, dx - \int_{\Omega} g^{(\eta)}(x) h(x) \cdot D(\bar{\varepsilon} \circ (I + u)) \, dx \right| \leq \|h\|_{C^1(\Omega)^d} \rho(\|h\|_{C^1(\Omega)^d}).
\]

(3.13)

Now, we have the following estimate:

\[
\left| \int_{\Omega} g^{(\eta)}(x) h(x) \cdot D(\bar{\varepsilon} \circ (I + u)) \, dx - \int_{\Omega} [\bar{\varepsilon}(x + u) - \varepsilon(x)] h(x) \cdot D(\bar{\varepsilon} \circ (I + u)) \, dx \right| \leq C\eta\|h\|_{C^1(\Omega)^d}.
\]

(3.14)

Indeed, since \( \bar{\varepsilon} \in C^k_\ast(\Omega) \subset SBV(\Omega), \bar{\varepsilon} \circ (I + u) \in SBV(\Omega) \) and we can write the following decomposition of \( D(\bar{\varepsilon} \circ (I + u)) \) into a continuous part and a jump part on a rectifiable surface \( S \):

\[
D(\bar{\varepsilon} \circ (I + u)) = \nabla (\bar{\varepsilon} \circ (I + u)) \mathcal{H}^d + [\bar{\varepsilon} \circ (I + u)]\nu_S \mathcal{H}^{d-1}_S,
\]
we have that
\[ \left| \int_\Omega [g^\eta(x) - [\tilde{\varepsilon}(x + u) - \varepsilon(x)]] h(x) \cdot \nabla (\tilde{\varepsilon} \circ (I + u)) (x) \, dx \right| \leq C_1 \eta \| h \|_{C^1(\Omega)^d}. \]

For the jump part, since \( S \) is a rectifiable surface and the function \( f^\eta = g^\eta - [\tilde{\varepsilon} \circ (I + u) - \varepsilon] \) is piecewise continuous, it is possible to define a trace \( f^\eta|_S \) on the surface \( S \) satisfying
\[ \| f^\eta|_S \|_{L^1(S)} \leq C_2 \| f^\eta \|_{L^1(\Omega)} \]
for some positive constant \( C_2 \) depending only on \( S \) and \( \Omega \). Then we get
\[ \left| \int_S f^\eta h(x) \cdot [\tilde{\varepsilon} \circ (I + u)] \nu S dH^d_S \right| \leq C_3 \eta \| h \|_{C^1(\Omega)^d} \]
for some positive constant \( C_3 \) independent of \( \eta \) and \( h \).

Now, the last term \( \int_\Omega [\tilde{\varepsilon}(x + u + h) - \tilde{\varepsilon}(x + u)]^2 \) can be handled using Lemma 3.8. Doing so, we obtain
\[ \int_\Omega [\tilde{\varepsilon}(x + u + h) - \tilde{\varepsilon}(x + u)]^2 = \int_\Omega \tilde{\varepsilon}_2^2(x + u) |h \cdot \nu| \delta_{\partial \tilde{\Omega}_2} (x + u) + o(\| h \|_{C^1(\Omega)^d}). \quad (3.15) \]

Combining (3.12), (3.13), (3.14), and (3.15), we get that for every \( \eta > 0 \),
\[ \left| I(u+h) - I(u) - 2 \int_\Omega [\tilde{\varepsilon}(x+u) - \varepsilon(x)] h(x) \cdot D\tilde{\varepsilon} \circ (I+u)(x) \, dx - \int_\Omega \tilde{\varepsilon}_2^2(x+u) |h \cdot \nu| \delta_{\partial \tilde{\Omega}_2} (x+u) \, dx \right| \leq C_4 \| h \|_{C^1(\Omega)^d} \left( \rho(\| h \|_{C^1(\Omega)^d}) + \eta \right) \]
for some positive constant \( C_4 \) independent of \( h \) and \( \eta \).

Finally, it follows that
\[ I(u + h) - I(u) = (\xi, h) + \int_\Omega \tilde{\varepsilon}_2^2(x + u) |h \cdot \nu| \delta_{\partial \tilde{\Omega}_2} (x + u) \, dx + o(\| h \|_{C^1(\Omega)^d}), \]
where \( \xi \) is defined by (3.8). Hence, either \( \int_\Omega \tilde{\varepsilon}_2^2(x + u) |h \cdot \nu| \delta_{\partial \tilde{\Omega}_2} (x + u) \, dx \) is of order of \( \| h \|_{C^1(\Omega)^d} \) and we get
\[ I(u + h) - I(u) \geq (\xi, h) \]
for \( \| h \|_{C^1(\Omega)^d} \) small enough or \( \int_\Omega \tilde{\varepsilon}_2^2(x + u) |h \cdot \nu| \delta_{\partial \tilde{\Omega}_2} (x + u) \, dx = o(\| h \|_{C^1(\Omega)^d}) \) and in this case, \( I \) is Fréchet differentiable and \( \xi \) is its Fréchet derivative. The proof of Proposition 3.5 is then complete. \( \square \)

**Remark 3.9** The minimization of the functional \( I \) gives a reconstruction of \( u^* \) on a subdomain \( \Omega \subset \Omega_0 \). In practical conditions, since \( u^* \) is small \( \Omega \) is almost the whole domain \( \Omega_0 \). The values of \( u^* \) on the boundary are known and, since \( u^* \) is of class \( C^1 \), it is possible to deduce the values of \( u^* \) on \( \Omega_0 \setminus \Omega \) by interpolation.
4 Reconstruction of the shear modulus

The problem is now to recover the function $\mu$ the reconstructed internal data $u$. For doing so, we use the method described in [4]. We introduce the operator $F$

$$u = F[\mu] = \begin{cases} \nabla \cdot (\mu (\nabla u + \nabla u^T)) + \nabla p = 0 & \text{in } \Omega_0, \\ \nabla \cdot u = 0 & \text{in } \Omega_0, \\ u = f & \text{on } \partial \Omega_0, \end{cases}$$

and minimize the function $K$ given by

$$K[\mu] = \frac{1}{2} \int_{\Omega_0} |F[\mu] - u|^2 \, dx.$$ 

According to [4], $K$ is Fréchet differentiable and its gradient can be explicitly computed. Let $v$ be the solution of

$$\begin{cases} \nabla \cdot (\mu (\nabla v + \nabla v^T)) + \nabla q = (K[\mu] - u) & \text{in } \Omega_0, \\ \nabla \cdot v = 0 & \text{in } \Omega_0, \\ v = 0 & \text{on } \partial \Omega_0. \end{cases}$$

Then,

$$\nabla K[\mu][h] = \int_{\Omega_0} h(\nabla v + \nabla v^T) : (\nabla u + \nabla u^T) \, dx.$$ 

A gradient descent method can be applied in order to reconstruct $\mu$ from $u$. We refer to [4] for more details.

5 Numerical experiments

We take $\Omega = [0, 1]^2$ and discretize it on a $300 \times 300$ grid, and generate a random Gaussian process to model the optical index $\varepsilon$ of the medium as shown in Figure 5.1. Given a shear modulus $\mu$ map on $\Omega$; see Figure 5 (left), we solve (1.1) on $\Omega$ via a finite element method compute the displacement field $u$. We then compute the displaced optical index $\varepsilon u$ by using a spline interpolation approach and proceed to recover the shear modulus from the data $\varepsilon$ and $\varepsilon u$ on the grid by the method described in the paper.

Using (3.5), we first compute the initial guess $u_\delta$ for the displacement field as the least-square solution to minimization of $J_x$. Figure 5.2 shows the kernel $w_\delta$ used to compute $u_\delta$. As one can see $\delta$ needs to be large enough so the matrix $w_\delta * (\nabla \varepsilon \nabla \varepsilon^T)$ is invertible at each point $x$, which is basically saying that $\delta$ must be bigger than the correlation length of $\varepsilon$. Figure 5.3 shows the conditioning of the matrix $w_\delta * (\nabla \varepsilon \nabla \varepsilon^T)$. Figure 5.4 shows the true displacement $u^*$, the result of the first order approximation (i.e., the initial guess) $u_\delta$ and then the result of the optimization process using a gradient descent method to minimize the discrepancy functional $I$.

Once the displacement inside the domain is reconstructed, we can recover the shear modulus $\mu$, as shown in Figure 5. We reconstruct $\mu$ by minimizing the functional $K$ and using a gradient descent-type method. Note that gradient of $K$ is computed with the adjoint state method, described previously. As it can be seen in Figure 5, the reconstruction is very accurate but not so perfect on the boundaries of $\Omega$, which is due to the poor estimation of $u$ on $\partial \Omega$. 

13
Figure 5.1: Optical index $\varepsilon$ of the medium.

Figure 5.2: Averaging kernel $w_5$.

6 Concluding remarks

In this paper, we developed a novel algorithm which gives access not only to stiffness quantitative information of biological tissues but also opens the way to other contrasts such as mechanical anisotropy. In the heart, the muscle fibers have anisotropic mechanical properties. It would be very interesting to detect a change in fiber orientation using OCT elastographic tomography.

References

[1] G. Alberti and C. Mantegazza, A note on the theory of SBV functions, Boll. Un. Mat. Ital., B 11 (1997), 375–382.

[2] L. Ambrosio, N. Fusco, and D. Pallara, Functions of Bounded Variation and Free Discontinuity Problems, Clarendon Press Oxford, 2000.
Figure 5.3: Conditioning of the matrix $w_δ \star \nabla \varepsilon \nabla \varepsilon^T$.

Figure 5.4: Displacement field and its reconstruction.
Figure 5.5: Shear modulus reconstruction.

[3] H. Ammari, An Introduction to Mathematics of Emerging Biomedical Imaging, Math. Appl., Vol. 62, Springer-Verlag, Berlin, 2008.

[4] H. Ammari, E. Bretin, J. Garnier, H. Kang, H. Lee, and A. Wahab, Mathematical Methods in Elasticity Imaging, Princeton Series in Applied Mathematics, Princeton University Press, 2014.

[5] H. Ammari, P. Garapon, H. Kang, and H. Lee, A method of biological tissues elasticity reconstruction using magnetic resonance elastography measurements, Quart. Appl. Math., 66 (2008), 139–175.

[6] J.F. Canny, A computational approach to edge detection, IEEE Trans. Pattern Anal. Mach. Intell., 8 (1986), 679–697.

[7] Y.Z. Chen and L.C. Wu, Second Order Elliptic Equations and Elliptic Systems, Translated from the 1991 Chinese original by Bei Hu. Translations of Mathematical Monographs, 174. American Mathematical Society, Providence, RI, 1998.

[8] F.H. Clarke, Yu. S. Ledyaev, R.J. Stern, and P.R. Wolenski, Nonsmooth Analysis and Control Theory, Graduate Texts in Mathematics, Springer-Verlag, New York, 1998.

[9] A. Dubois and A.C. Boccara, Full-field optical coherence tomography, in Optical Coherence Tomography, 565–591, Biological and Medical Physics, Biomedical Engineering, Springer, 2008.

[10] A. Dubois, K. Grieve, G. Moneron, R. Lecaque, L. Vabre, and C. Boccara, Ultrahigh-resolution full-field optical coherence tomography, Appl. Optics, 43 (2004), 2874–2883.

[11] P. Elbau, L. Mindrinos, and O. Scherzer, Mathematical modeling of optical coherence tomography, arXiv: 1403.0726.
[12] M. Giaquinta and L. Martinazzi, An Introduction to the Regularity Theory for Elliptic Systems, Harmonic Maps and Minimal Graphs, Second edition. Appunti. Scuola Normale Superiore di Pisa (Nuova Serie), 11. Edizioni della Normale, Pisa, 2012.

[13] Y.Y. Li and L. Nirenberg, Estimates for elliptic systems from composite material. Dedicated to the memory of Jürgen K. Moser, Comm. Pure Appl. Math., 56 (2003), 892–925.

[14] X. Liang, V. Crecea, and S. Boppart, Dynamic optical coherence elastography: A review, J. Innov. Opt. Health Sci., 3 (2010), 221–233.

[15] A. Manduca, T.E. Oliphant, M.A. Dresner, J.L. Mahowald, S.A. Kruse, E. Amromin, J.P. Felmlee, J.F. Greenleaf, and R.L. Ehman, Magnetic resonance elastography: Non-invasive mapping of tissue elasticity, Med. Imag. Anal., 5 (2001), 237–254.

[16] R. Muthupillai and R.L. Ehman, Magnetic resonance elastography, Nat. Med., 2 (1996), 601–603.

[17] W. Naetar and O. Scherzer, Quantitative photoacoustic tomography with piecewise constant material parameters, arXiv:1403.2620.

[18] A. Nahas, M. Bauer, S. Roux, and A.C. Boccara, 3D static elastography at the micrometer scale using Full Field OCT, Biomedical Opt. Expr., 4 (2013), 2138–2149.

[19] M. Razami, A. Mariampillai, C. Sun, V.X.D. Yang, and M.C. Kolios, Biomechanical properties of soft tissue measurement using optical coherence elastography, Proc. SPIE, 8207 (2012), 820758.

[20] J. Rogowska, N.A. Patel, J.G. Fujimoto, and M.E. Brezinski, Optical coherence tomographic elastography technique for measuring deformation and strain of atherosclerotic tissues, Heart, 90 (2004), 556–562.

[21] J.M. Schmitt, OCT elastography: imaging microscopic deformation and strain in tissue, Opt. Express, 3 (1998), 199–211.

[22] J.K. Seo and E.J. Woo, Nonlinear Inverse Problems in Imaging, Wiley, 2013.