The ‘critical trochanter angle’ does not show superiority over the CCD angle in predicting varus stem alignment in cementless short-stem total hip arthroplasty

Matthias Luger1,2 · Sandra Feldler1,2 · Lorenz Pisecky1,2 · Jakob Allerstorfer1,2 · Tobias Gotterbarm1,2 · Antonio Klasan1,2

Received: 9 July 2021 / Accepted: 3 January 2022 / Published online: 12 January 2022
© The Author(s) 2022

Abstract
Purpose Varus positioning of the femoral stem can affect the hip offset (HO). The critical trochanter angle (CTA) was introduced in 2019 as a novel geometric angle, to predict varus stem alignment in cementless straight stem THA. The aim of this study was to evaluate the applicability of the CTA as a predictor for stem alignment in THA with a cementless neck resecting short stem.

Patients and methods In this retrospective study, 106 patients (index surgery 2014–2019) with unilateral THA and a morphologically healthy contralateral hip as a reference (Kellgren–Lawrence ≤ 1) were included. A cementless short stem with meta-diaphyseal fixation and press-fit cup was implanted in all cases. Stem alignment, CCD angle, CTA and offset reconstruction were measured on preoperative and 3 months postoperative AP radiographs of the pelvis.

Results Preoperative lower CTA and lower CCD angle were positively correlated ($r=0.472; p<0.001$). Higher varus stem alignment is correlated with lower CTA ($r=-0.384; p<0.001$) and lower CCD angle ($r=-0.474; p<0.001$). A CTA of 23.1° or lower showed a sensitivity of 59.1% and a specificity of 87.1% (AUC: 0.733) and a CCD angle of 132.75° or lower a sensitivity of 68.2% and a specificity of 80.6% (AUC: 0.77) for a varus stem alignment >3°.

Conclusion The CTA is also applicable in cementless THA with a neck resecting short stem to evaluate risk of intraoperative varus stem positioning. The CCD angle shows higher sensitivity with marginally lower specificity. Therefore, the CTA is not superior in predicting varus stem alignment in short-stem THA.

Level of evidence IV.

Keywords Critical trochanter angle · Stem alignment · Short stem · Total hip arthroplasty · THA · Fitmore · Anterolateral approach
Introduction

Correct reconstruction of femoro-acetabular offset and leg length are clinically important factors in total hip arthroplasty (THA) [1]. Conventional straight stems show excellent long-term outcomes [2], but have the disadvantage of limited ability to restore the femoral offset (FO) due to their straight stem design [3]. Restoration of the native FO increases postoperative range of motion, abductor muscle function and decreases polyethylene wear [3–5]. Varus malalignment of the femoral stem in the coronal plane may affect offset or leg length restoration and can hamper optimum load transfer between the implant and natural bone [6].

Haversath et al. [7] have introduced a novel geometric angle named ‘critical trochanter angle’ (CTA) as a predictor for stem alignment. A low CCD angle and a long neck and a trochanter overhand enhance the risk for intraoperative varus stem positioning [7, 8]. The CTA measures the extent of the trochanter overhang in relation to the femoral shaft axis [7]. A CTA lesser or equal to 22.75° showed a sensitivity of 90% and a specificity of 80% for a varus stem position of 2° or greater [7].

The CTA was described in cementless THA with a cementless collarless straight stem design with a narrow shoulder [7]. In recent years, cementless short stems have been increasingly used [1, 9, 10]. Short stems show advantages in the reconstruction of femoro-acetabular offset [1, 11], are superior in preservation of proximal bone stock [12], and facilitate minimally invasive surgery [9, 13]. A short curved stem can initially be inserted in a more varus position following a c-shaped path [9]. However, the final position of a short stem depends on the stem design, fixation, and the level of the neck osteotomy. In case of a neck resecting short stem [14], the aim of the final implantation is oriented in line with the diaphysis [9].

As the insertion of a neck resecting short stem is initially in a more varus position, the risk for final varus malalignment exists. Therefore, this study was conducted to evaluate, if the CTA is also applicable as a predictor for stem alignment in THA with a cementless neck resecting short stem.

Methods

Patients

This retrospective radiological comparative study includes patients of a consecutive series of THAs with the same cementless curved short stem (Fitmore® stem, ZimmerBiomet, Warsaw, IN, USA) and bi-hemispherical press-fit acetabular cup (Allofit®/-S, ZimmerBiomet) performed via a minimally invasive supine anterolateral approach. Fitmore® hip stem is a titanium alloy stem (Ti Al6V4) that has a Porolock Ti-VPS coating in the proximal part to enhance bone ingrowth and is available in four different neck angle options (127°, 129°, 137°, 140°) and 14 different sizes (size 1–14) for each offset option [9]. A cementless titanium press-fit cup with or without screws (Allofit®/-S, ZimmerBiomet, Warsaw, IN, USA) was used in all patients.

A consecutive series of 1052 hips in 982 patients with index surgery between 2014 and 2019 were screened for inclusion and the medical records until 90 days postoperative were evaluated. The preoperative X-rays of the pelvis (both hips in comparison, anterior–posterior view, standing upright) were screened for unilateral THA. Diagnoses for inclusion were primary osteoarthritis, avascular necrosis of the femoral head or mild dysplasia of the hip (Crowe I) [15]. Exclusion criteria were defined as bilateral hip disease (Kellgren–Lawrence > grade 1) [16], a history of prior hip surgery, previous trauma, postoperative complication, reoperation, or revision for any reason as well as missing preoperative or postoperative radiographs. In total, 106 patients met the inclusion criteria.

Radiographic measurements were performed on preoperative and 3 months postoperative low centered anteroposterior (AP) radiographs of the pelvis in both groups. Preoperative age at operation, gender, body mass index (BMI), and laterality were recorded.

The study was approved by the institutional review board (EK-No.: 1239/2019). Due to the retrospective study design with evaluation of pre-existing medical records, informed consent was not required. All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards.

Surgical technique and treatment protocol

Surgical procedures were carried out at the author’s institution by surgeons with different levels of experience including 11 consultants and 7 residents. All consultants perform more than 50 and all senior consultants more than 100 arthroplasties per year. Resident surgeries were done under the guidance of a consultant. In all cases, a minimally invasive anterolateral Watson–Jones approach in supine position on a standard operating table under laminar airflow was performed. Extremity preparation was performed with threefold antiseptic scrub with alcohol disinfectant. Draping with a sterile adhesive surgical iodine film was used. The skin incision was centered over the greater trochanter. An incision at
the border between the tensor fasciae latae and the tractus iliotibialis was performed. Then the Watson–Jones interval between tensor fasciae latae und gluteus medius was bluntly dissected. A capsulectomy was performed in every case. Fluoroscopy was routinely used with the definitive cup and trial stem in situ. The standardized peri- and postoperative protocol was identical in all cases, including single-shot antibiotics (Cefuroxime 1.5 g i.v. directly preoperative), weight-bearing as tolerated from the first postoperative day on, indomethacin 75 mg daily for the prevention of heterotopic ossification on day 1–4 postoperatively and 40 mg low-molecular weight heparin or Rivaroxaban 10 mg for 28 days postoperatively as venous thromboembolic event prophylaxis.

**Radiographic evaluation**

Radiographic measurement was performed on preoperative and 3 months postoperative digital low-centered AP radiographs of the pelvis [17]. Measurements were conducted independently by two reviewers (M.L., J.A.), who were not involved in the index surgery. Radiographs were taken with the patient in standing position and with both legs in 15° internal rotation with the central beam directed on the symphysis pubis [18]. To achieve an accurate measurement of the hip anatomy a double coordinate system was applied on both the preoperative and the postoperative images [1, 19]. Radiographic analysis was performed using MediCAD® Software V5.1 (Hectec GmbH, Germany). The hip center of rotation (COR) was defined using a circle tool determining the diameter of the femoral head and its center [20]. The femoral offset (FO) was determined as the perpendicular distance between the COR and the proximal femoral shaft axis (FSA) [17, 20]. Acetabular offset (AO) was measured as the perpendicular distance between the COR and line T, with T being the perpendicular line on the transteardrop line (TT) through the ipsilateral teardrop figure [17]. Hip offset (HO) was calculated as the sum of FO and AO [17]. The vertical position of the COR was measured as the perpendicular distance to line TT [21]. Radiographic leg length discrepancy (LLD) was measured as the perpendicular distance between line TT and the middle of the lesser trochanter (LT) [18]. Centrum–collum–diaphyseal (CCD) angle was determined according to M. E. Müller on the affected hip [22]. Definition of the stem axis of the implanted cementless stem was previously described for cementless straight stem [23] and for Fitmore® hip stem [24]. For enabling exact measurement of the stem axis of the implanted Fitmore® stem, a digital template of the stem size was put over the implanted stem on the postoperative X-ray. The templating software displayed the correct stem axis of the implanted Fitmore® hip stem, Fig. 3. The critical trochanter angle (CTA) was measured as described by Haversath et al. [7]. The angle crest is defined as the intersection of the femoral shaft axis and the femoral neck axis. A leg between the angle crest and the trochanter vertex is built, and the CTA is measured between this leg and the femoral shaft axis, Fig. 1. To characterize the anatomical shape of the proximal femur and the thickness of cortical bone, the canal to calcar isthmus ratio and the cortical index (CI) according to Dorr et al. [25] were determined. A high CI indicates a thick cortical bone [25]. Additionally, the canal flare according to Noble et al. [26] was determined. The stem alignment was measured as the difference in degrees between the anatomic femoral shaft axis and the vertical stem axis [27]. On preoperative X-rays FO, AO, HO and LLD were measured bilaterally, while CCD angle, CI, Canal Flare Index and canal to calcar ratio were measured unilaterally on the affected hip. Complete preoperative measurements are also shown in Fig. 2.

On postoperative X-rays FO, AO, HO and LLD were measured bilaterally, while stem alignment was measured unilaterally on the operated hip. Complete postoperative measurements are also shown in Fig. 3.

Intra- and interobserver reliabilities were calculated. Intra-class correlation coefficients (ICC) were used with a two-way random effects model for absolute agreement. Repeated measurements for intraobserver reliability were performed at day 1 and day 14 in a blinded fashion.

**Statistical analysis**

Descriptive statistical analysis was conducted for age, gender, body mass index (BMI) and laterality, as well as measurements for FO, AO, HO, LLD, Canal Flare Index, CI, canal to calcar ratio, stem alignment, CCD angle and CTA. Power analysis was not performed due to the observed statistical significance for the primary endpoint [28]. An ANOVA was conducted for testing differences in
Fig. 2 Preoperative measurements: HO, FO, AO, LLD (all bilaterally), CTA, CCD angle, Canal Flare Index, Cortical Index, canal to calcar ratio (all unilaterally)

Fig. 3 Postoperative measurements: HO, FO, AO, LLD (all bilaterally), stem alignment (unilaterally)
CCD-Angle, CTA and stem alignment. Pearson’s coefficient was used for the correlation of CCD angle and CTA with preoperative FO and HO, Canal Flare Index, CI and canal to calcar ratio. Additionally, a Pearson’s coefficient was used for the correlation of CTA, CCD angle, and stem alignment with postoperative difference in HO and FO to the contralateral side and leg length difference. Preoperative and postoperative differences in HO, FO, and AO were always calculated in relation to the contralateral healthy hip. A receiver operating characteristics (ROC) curve was calculated to obtain an analysis for sensitivity and specificity of CTA und CCD cutoff values that result in varus stem alignment greater than 3°, with the reported area under the curve (AUC) (Fig. 4). The Youden Index was used to define the optimal cut-point [29]. Statistical analysis was performed with SPSS version 27 (IBM SPSS statistics, Chicago, IL, USA). A p value < 0.05 was considered as statistically significant.

### Results

The intraobserver interclass correlation coefficient between the two sets of measurements was 0.992% (95% confidence interval 0.987–0.994, P < 0.001).

The patient demographics are shown in Table 1. Average CCD angle and CTA were significantly lower (p < 0.001) in patients with varus stem alignment, Table 2. FO and HO differences were also significantly higher (p = 0.006; p = 0.024) in patients with postoperative varus stem alignment. A significant correlation was found for CTA and CCD angle, preoperative FO and HO, Table 3. A lower CTA was

### Table 1 Patient demographics

|                     |        |
|---------------------|--------|
| Number of patients  | 106    |
| Gender (male:female)| 41:65  |
| Side (left:right)   | 49:57  |
| Age at operation (years) | 57.11 ± 11.17 |
| BMI (kg/m²)         | 27.61 ± 4.95 |

![ROC Curve](source_of_the_curve.png)  
**Fig. 4** ROC curve for CCD angle and CTA for varus stem alignment > 3°
correlated with lower CCD angle ($r=0.472; p<0.001$). A negative correlation was found for CTA and preoperative FO ($r=-0.522; p<0.001$) and HO ($r=-0.421; p<0.001$), meaning a lower CTA correlated with higher preoperative FO and HO. A significant correlation for CCD angle and CTA ($r=0.472; p<0.001$), preoperative FO ($r=-0.569; p<0.001$), HO ($r=-0.418; p<0.001$), Canal Flare Index ($r=-0.252; p=0.009$), Cortical Index ($r=-0.418; p<0.001$) and canal to calcar ratio ($r=0.219; p=0.024$) was found.

Table 4 shows the correlation for postoperative measurements. A lower CTA is significantly correlated with a lower CCD angle ($r=0.472; p<0.001$) and with higher varus stem alignment ($r=-0.384; p<0.001$). A lower CCD angle is correlated with higher varus stem alignment ($r=-0.474; p<0.001$). Higher varus stem alignment is significantly correlated with lower CTA ($r=-0.384; p<0.001$) and CCD angle ($r=-0.474; p<0.001$). A significant correlation is also for increased postoperative FO ($r=0.724; p<0.001$) and HO ($r=0.357; p<0.001$).

The ROC analysis showed an AUC of 0.77 for CCD angle and 0.733 for CTA for a varus stem alignment $>3°$. The Youden Index was highest for a CTA of 23.1° with a sensitivity of 59.1% and a specificity of 87.1% for a varus stem alignment $>3°$. The Youden Index was highest for a CCD angle of 132.75° with a sensitivity of 68.2% and a specificity of 80.6% for a varus stem alignment $>3°$.

### Discussion

A lower CTA and CCD angle is significantly correlated with higher varus stem alignment in cementless THA with a neck resecting short curved stem. Additionally, higher varus stem alignment leads to significantly higher increase in FO and HO compared to a contralateral healthy hip as reference. Also, a positive correlation is found for higher varus stem alignment and postoperative FO and HO difference.

**Table 2** Preoperative and postoperative measurements

| Measure                   | Preoperative | Postoperative |
|---------------------------|--------------|---------------|
| FO preoperative (mm)      | 39.46 ± 6.67 |               |
| FO difference preoperative (mm) | 1.93 ± 4.12 |               |
| AO preoperative (mm)      | 34.58 ± 4.43 |               |
| AO difference preoperative (mm) | 0.82 ± 2.46 |               |
| HO preoperative (mm)      | 74.04 ± 8.48 |               |
| HO difference preoperative (mm) | 1.11 ± 4.08 |               |
| Canal flare index         | 3.91 ± 0.633 |               |
| Cortical index            | 0.6 ± 0.05  |               |
| Calcar to canal ratio     | 0.57 ± 0.07 |               |

**Stem alignment (°)**

| Alignment | Count (%) | Mean ± SD |
|-----------|-----------|-----------|
| 0°–1°     | 18 (17.0%) | 3.1 ± 4.65 |
| > 1–5°    | 44 (41.5%) | 20.07 ± 6.88 |
| > 5°      | 44 (41.5%) | 24.41 ± 7.93 |
| CTA (°)   |           |           |
| 0°–1°     |           | 0.472     |
| > 1–5°    |           | −0.522    |
| > 5°      |           | −0.421    |
| CCD (°)   |           |           |
| 0°–1°     |           | 0.472     |
| > 1–5°    |           | −0.569    |
| > 5°      |           | −0.418    |
| FO difference postoperative (mm) | 2.92 5.39 | 0.024    |
| 0°–1°     |           |           |
| > 1–5°    |           | 0.44 5.2  |
| > 5°      |           | 2.48 4.54 |
| AO difference postoperative (mm) | − 3.81 4.15 | 0.028    |
| 0°–1°     |           |           |
| > 1–5°    |           | − 3.81 4.15 |
| > 5°      |           | − 3.81 4.15 |

**Table 3** Correlation of preoperative measurements with CTA and CCD angle

| Measure       | CTA | CCD angle | FO preoperative | HO preoperative | Canal flare index | Cortical index | Calcar to calcar ratio |
|---------------|-----|-----------|-----------------|-----------------|-------------------|---------------|------------------------|
| Pearson’s $r$ | 0.472 | − 0.522 | − 0.421 | − 0.080 | − 0.147 | 0.011 |
| $P$ value     | < 0.001 | < 0.001 | < 0.001 | 0.414 | 0.131 | 0.911 |
| Pearson’s $r$ | 0.472 | − 0.569 | − 0.418 | − 0.252 | − 0.418 | 0.219 |
| $P$ value     | < 0.001 | < 0.001 | < 0.001 | 0.009 | < 0.001 | 0.024 |
Haversath et al. [7] initially described the CTA as a predictor for risk of varus stem alignment in cementless THA with a cementless collarless straight stem design with a narrow shoulder for direct anterior approach (DAA) and lateral Hardinge approach. A statistically significant correlation was found for CTA and CCD angle. A coxa vara deformity was significantly correlated with lower CTA [7]. Murphy et al. [8] also described a higher varus stem alignment in cementless straight stem THA in patients with coxa vara deformity. The results in the present study show comparable findings. A significant correlation between lower CTA and lower CCD angle was also found.

A lower CTA is negatively correlated with higher varus stem alignment in straight stem THA [7]. A lower CCD angle is also negatively correlated with higher varus stem alignment [7, 8]. These findings are also applicable in short-stem THA. Our results show similar statistically significant correlations between CCD angle, CTA and stem alignment. Therefore, a lower CCD angle and CTA are also possible risk factors for varus stem alignment in cementless short-stem THA with a neck resecting short stem. Although the stem used in this study has a C-shaped curvature, designed to minimize varus malalignment, this study demonstrates that it nevertheless does occur, with the risks being similar to those for the straight cementless stems.

The cut-off of 22.75° or less for the CTA showed a sensitivity of 90° and specificity of 80° for varus stem alignment of 2° or greater in straight stem THA [7]. We detected a cut-off for the CTA for a varus stem alignment > 3° of 23.1° with a sensitivity of 59.1% and a specificity of 87.1%. A cut-off of 132.75° for the CCD angle showed a higher sensitivity with minimally lower specificity. These findings are also applicable in short-stem THA with a neck resecting short stem. Although the stem used in this study has a C-shaped curvature, designed to minimize varus malalignment, this study demonstrates that it nevertheless does occur, with the risks being similar to those for the straight cementless stems.

A statistically significant correlation was found for CTA and CCD angle. A coxa vara deformity was significantly correlated with lower CTA [7]. Murphy et al. [8] also described a higher varus stem alignment in cementless straight stem THA in patients with coxa vara deformity. The results in the present study show comparable findings. A significant correlation between lower CTA and lower CCD angle was also found.

The results in the presented study show a statistically significant difference in postoperative HO and FO difference with higher varus stem alignment and postoperative leg length difference could not be found. Testing for postoperative HO and FO difference resulted in a statistically significant difference in postoperative HO and FO difference with higher varus stem alignment with > 1° or > 5° of varus placement of the femoral stem. A postoperative difference in HO ≥ 5 mm compared to a contralateral hip is associated with poorer delta gain in Harris Hip Score (HHS). These significantly lower delta gains increase with every 2.5 mm increase above 5 mm. The results in the presented study show an increase in postoperative HO of 2.48 mm (± 4.54 mm) and 4.39 mm (± 5.89 mm) in patients with varus positioning between > 1° and 5° of varus placement of the femoral stem. A postoperative difference in HO ≥ 5 mm compared to a contralateral healthy hip as reference. A correlation between higher varus stem alignment and postoperative leg length difference could not be found. Testing for postoperative HO and FO difference resulted in a statistically significant difference in postoperative HO and FO difference with higher varus stem alignment with > 1° or > 5° of varus placement of the femoral stem. A postoperative difference in HO ≥ 5 mm compared to a contralateral hip is associated with poorer delta gain in Harris Hip Score (HHS). These significantly lower delta gains increase with every 2.5 mm increase above 5 mm. The results in the presented study show an increase in postoperative HO of 2.48 mm (± 4.54 mm) and 4.39 mm (± 5.89 mm) in patients with varus positioning between > 1° and 5° and > 5°. Therefore, the clinical impact of higher varus stem positioning might be without high clinical relevance. These results are similar compared to previous studies, reporting a moderate increase in HO and FO with a varus alignment of Fitmore® stem ≥ 3° [30]. Additionally, a mild varus stem alignment of a cementless short stem does not lead to an increased risk of periprosthetic fracture [31]. As the impact of mild varus stem alignment leads to minor increases in HO and might not lead an increased risk in perioperative complications it might be rather radiographically unsatisfying.

Table 4 Correlation of postoperative measurements and BMI with CTA, CCD angle and stem alignment

| CTA  | CCD  | Stem alignment | HO difference post-OP | FO difference post-OP | Leg length difference | BMI |
|------|------|----------------|------------------------|------------------------|-----------------------|-----|
| Pearson’s r | 0.472 | − 0.384 | <0.000 | − 0.031 | − 0.024 | 0.103 |
| P value | < 0.001 | < 0.001 | 0.999 | 0.751 | 0.807 | 0.294 |
| CCD  | CTA  | Stem alignment | HO difference post-OP | FO difference post-OP | Leg length difference | BMI |
| Pearson’s r | 0.472 | − 0.474 | − 0.056 | 0.022 | 0.028 | 0.032 |
| P value | < 0.001 | < 0.001 | 0.567 | 0.823 | 0.777 | 0.746 |
| Stem alignment | CTA  | CCD  | HO difference post-OP | FO difference post-OP | Leg length difference | BMI |
| Pearson’s r | − 0.384 | − 0.474 | 0.357 | 0.724 | − 0.077 | − 0.175 |
| P value | < 0.001 | < 0.001 | <0.001 | <0.001 | 0.435 | 0.072 |

Bold letters for significant values.
rather than clinically important. However, our results do not include patient-orientated outcome measurements (PROMs) and, therefore, a final verdict cannot be given with our presented data.

Several limitations of the study have to be addressed. First, we tried to minimize a potential selection bias with very strict inclusion criteria. Only patients with a single implant design and approach were included in this study. The results might not be applicable to other stem designs, although our results are similar to those with a straight stem. A homogenous study cohort was created by excluding patients with a bilateral hip disease (Kellgren–Lawrence > grade 1). Furthermore, we aimed to increase reliability of the measurements and results by restricting inclusion based on preoperative diagnosis. We excluded all forms of secondary osteoarthritis of the hip and development dysplasia of the hip Crowe grade II to IV. Prior surgery before THA was also excluded. However, mild hip dysplasia (lateral center–edge angle 20–25°), coxa profunda, and morphologic alterations related to cam- or pincer-type impingement were included, because these changes might be subtle and cannot be reliably identified in the present study cohort with end-stage disease. Therefore, we conclude that the findings in the present study are applicable for primary osteoarthritis and care must be taken when applying our findings on secondary osteoarthritis or high grades of development dysplasia of the hip. Second, we address the fact of taking measurements on plain radiographs. FO is underestimated by approximately 13% on plain radiographs [20]. However, our measurements are easily reproducible, applicable in daily routine and less invasive regarding radiation exposure. Furthermore, we postulate variances in inter- and intraobserver reliability in measuring clinical leg length difference. Additionally, this study lacks of missing clinical outcome scores or PROMs. However, aim of this study was to find out, if the CTA is also applicable in cementless short-stem THA, which could be achieved by the presented data. We are fully aware that further research is necessary to any clinical relevance of varus placement of cementless short stems.

Conclusion

The CTA is also applicable in cementless THA with a neck resecting short stem to evaluate risk of intraoperative varus stem positioning. The CCD angle shows higher sensitivity with marginally lower specificity. Therefore, the CTA is not superior in predicting varus stem alignment in short-stem THA.

Author contributions ML: wrote the manuscript, performed the statistical analysis, designed the study, acquisition of data, and interpretation of the data. SF: involved in the acquisition of data and interpretation of the data. JA: revised the manuscript. TG: revised the manuscript. AK: jointly conceived the study, performed statistical analysis, and edited the manuscript.

Funding Open access funding provided by Johannes Kepler University Linz. The study was conducted without any funding or benefits from a commercial party. Three co-authors have received or will receive benefits for personal or professional use from a commercial party outside the conduction of this study.

Availability of data and materials Data and materials are available on request.

Declarations

Conflict of interest We report personal fees paid to one co-author (T.G.) during the conduct of the study from Zimmer Biomet, Europe and from Depuy Synthes Orthopädie GmbH, Peter Brehm GmbH, ImplanTec GmbH outside the submitted work. We report research grants paid to our institution during the conduct of the study from Zimmer Biomet, Europe, Mathys AG Switzerland, Anika Therapeutics outside the submitted work.

Ethical approval This study received ethical approval from the local institutional review board of the “Ethikkommission OÖ” of the Johannes Kepler University Linz (JKU Linz) (EK-No.: 1239/2019).

Consent to participate The study was approved by the institutional review board (EK-No.: 1239/2019) in accordance with the World Medical Association Declaration of Helsinki. Because of the retrospective evaluation of pre-existing medical records, an informed consent was not required.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article’s Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article’s Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/.

References

1. Kutzner KP, Kovacevic MP, Roeder C, Rebhein P, Pfeil J (2015) Reconstruction of femoro-acetabular offsets using a short-stem. Int Orthop 39(7):1269–1275. https://doi.org/10.1007/s00264-014-2632-3
2. Pisecky L, Hipmair G, Schauer B, Bohler N (2018) 30-years of experience with the cementless implanted Alloclassic total hip arthroplasty system—an ultra-long-term follow-up. J Orthop 15(1):18–23. https://doi.org/10.1016/j.jor.2017.11.003
3. Snijders TE, van Erp JHJ, de Gast A (2019) Restoring femoral offset and leg length; the potential of a short curved stem in total hip

 Springer
arthroplasty. J Orthop 16(5):396–399. https://doi.org/10.1016/j.jor.2019.04.013
4. McGrory BJ, Morrey BF, Cahalan TD, An KN, Cabanela ME (1995) Effect of femoral offset on range of motion and abductor muscle strength after total hip arthroplasty. J Bone Jt Surg Br 77(6):865–869
5. Sakalkale DP, Sharkey PF, Eng K, Hozack WJ, Rothman RH (2001) Effect of femoral component offset on polyethylene wear in total hip arthroplasty. Clin Orthop Relat Res 388:125–134. https://doi.org/10.1097/00003086-200107000-00019
6. Fottner A, Woiczinski M, Kistler M, Schroder C, Schmidutz TF, Jansson V, Schmidutz F (2018) Varus malalignment of cementless hip stems provides sufficient primary stability but highly increases distal strain distribution. Clin Biomech (Bristol, Avon) 58:14–20. https://doi.org/10.1016/j.clinbiomech.2018.07.006
7. Haversath M, Busch A, Jager M, Tassemieer T, Brandenburger D, Serong S (2019) The “critical trochanter angle”: a predictor for stem alignment in total hip arthroplasty. J Orthop Surg Res 14(1):165. https://doi.org/10.1186/s13018-019-1206-x
8. Murphy CG, Bonnin MP, Desbiolles AH, Carrillon Y, Aїt Si Selmi T (2016) Varus will have varus; a radiological study to assess and predict varus stem placement in uncemented femoral stems. Hip Int 26(6):554–560. https://doi.org/10.5301/hipint.5000412
9. Gustke K (2012) Short stems for total hip arthroplasty: initial experience with the Fitmore stem. J Bone Joint Surg Br 94(11 Suppl A):47–51. https://doi.org/10.1302/0301-620X.94B11.30677
10. Lombardi AV Jr, Berend KR, Ng VY (2011) Stubby stems: good muscle strength after total hip arthroplasty. J Bone Jt Surg Br 94(4):477–482. https://doi.org/10.1007/s00402-007-0494-5
11. Reichert JC, von Rottkay E, Roth F, Renz T, Hausmann J, Kranz J, Rackwitz L, Noth U, Rudert M (2018) A prospective randomized comparison of the minimally invasive direct anterior surgical approach on component positioning in primary total hip arthroplasty. BMC Musculoskelet Disord 20(1):261. https://doi.org/10.1186/s12891-019-2645-6
12. Pipino F, Molfetta L (1993) Femoral neck preservation in total hip replacement. Ital J Orthop Traumatol 19(1):5–12
13. Gkagkalis G, Goetti P, Mai S, Meinecke I, Helmy N, Bosson D, Serong S (2019) Femoral offset is underestimated on anteroposterior radiographs of the pelvis but accurately assessed on anteroposterior radiographs of the hip. J Bone Jt Surg Br 94(4):477–482. https://doi.org/10.1007/s00402-007-0494-5
14. Gkagkalis G, Goetti P, Mai S, Meinecke I, Helmy N, Bosson D, Serong S (2019) The “critical trochanter angle”: a predictor for stem alignment in total hip arthroplasty. J Orthop Surg Res 14(1):165. https://doi.org/10.1186/s13018-019-1206-x
15. Crowe JF, Mani VJ, Ranawat CS (1979) Total hip replacement in congenital dislocation and dysplasia of the hip. J Bone Jt Surg Am 61(1):15–23
16. Kellgren JH, Lawrence JS (1957) Radiological assessment of osteo-arthritis. Ann Rheum Dis 16(4):494–502. https://doi.org/10.1136/ard.16.4.494
17. Dastane M, Dorr LD, Tarwala R, Wan Z (2011) Hip offset in total hip arthroplasty: quantitative measurement with navigation. Clin Orthop Relat Res 469(2):429–436. https://doi.org/10.1007/s11999-010-1554-7
18. Inmann MM, Streit MR, Kolb J, Heiland J, Parsch D, Aldinger PR, Konigshausen M, Gotterbarn T, Merle C (2015) Influence of surgical approach on component positioning in primary total hip arthroplasty. BMC Musculoskelet Disord 16:180. https://doi.org/10.1186/s12891-015-0623-1
19. Wedemeyer C, Quitmann H, Xu J, Heep H, von Knoch M, Saxler G (2008) Digital templating in total hip arthroplasty with the Mayo stem. Arch Orthop Trauma Surg 128(10):1023–1029. https://doi.org/10.1007/s00402-007-0494-5
20. Merle C, Waldstein W, Pegg E, Streit MR, Gotterbarn T, Aldinger PR, Murray DW, Gill HS (2012) Femoral offset is underestimated on anteroposterior radiographs of the pelvis but accurately assessed on anteroposterior radiographs of the hip. J Bone Jt Surg Br 94(4):477–482. https://doi.org/10.1007/s00402-016-20867
21. Inmann MM, Spier K, Streit MR, Aldinger PR, Bruckner T, Gotterbarn T, Merle C (2018) Comparative analysis of the reconstruction of individual hip anatomy using 3 different cementless stem designs in patients with primary hip osteoarthritis. J Arthroplasty 33(4):1126–1132. https://doi.org/10.1016/j.arth.2017.11.026
22. Waldt S, Eiber M, Wörtler K (2011) Messverfahren und Klassifikationen in der muskuloskeletalen Radiologie. Thieme, Stuttgart
23. Aldinger PR, Breusch SJ, Lukoschek M, Mau H, Ewerbeck V, Thomsen M (2003) A ten- to 15-year follow-up of the cementless spetroton stem. J Bone Joint Surg Br 85(2):209–214. https://doi.org/10.1302/0301-620X.85b2.13216
24. Inmann MM, Weishorn J, Bruckner T, Streit MR, Walker T, Gotterbarn T, Merle C, Maier MW (2019) Fifty-six percent of proximal femoral cortical hypertrophies 6 to 10 years after Total hip arthroplasty with a short Cementless curved hip stem—a cause for concern? BMC Musculoskelet Disord 20(1):261. https://doi.org/10.1186/s12891-019-2645-6
25. Dorr LD, Faugere MC, Mackel AM, Gruen TA, Bogner B, Maluchle HH (1993) Structural and cellular assessment of bone quality of proximal femur. Bone 14(3):231–242. https://doi.org/10.1016/8756-3282(93)90146-2
26. Noble PC, Alexander JW, Lindahl LJ, Yew DT, Granberry WM, Tullos HS (1988) The anatomic basis of femoral component design. Clin Orthop Relat Res 235:148–165
27. Aldinger PR, Jung AW, Breusch SJ, Ewerbeck V, Parsch D (2009) Survival of the cementless Spetroton stem in the second decade. Clin Orthop Relat Res 467(9):2297–2304. https://doi.org/10.1007/s11999-009-0906-7
28. Hoenig JM, Heisey DM (2001) The abuse of power. Am Stat 55(1):19–24. https://doi.org/10.1198/000313001300339897
29. Ruopp MD, Perkins NJ, Whitcomb BW, Schisterman EF (2008) Youden Index and optimal cut-point estimated from observations affected by a lower limit of detection. Biom J 50(3):419–430. https://doi.org/10.1002/bimj.200710415
30. Lugner M, Stiftinger J, Allerstorfer J, Hochgatterer R, Gotterbarn T, Pisecky L (2021) High varus stem alignment in short-stem total hip arthroplasty: a risk for reconstruction of femoro-acetabular offset, leg length discrepancy and stem undersizing? Arch Orthop Trauma Surg. https://doi.org/10.1007/s00402-021-04176-5
31. Nishioka ST, Andrews SN, Mathews K, Nakasone CK (2021) Varus malignment of short femoral stem not associated with post-hip arthroplasty fracture. Arch Orthop Trauma Surg. https://doi.org/10.1007/s00402-021-04244-w

Publisher's Note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.