Diagnostic value of intraluminal stent enhancement in estimating coronary in-stent restenosis

Mehdi Karami Nogourani, Maryam Moradi, Amirreza Sajjadieh Khajouei, Maryam Farghadani, Atefeh Eshaghian

Departments of 1Radiology and 2Cardiology, School of Medicine, Isfahan University of Medical Sciences, Isfahan, Iran.

*Corresponding author: Maryam Moradi, Department of Radiology, School of Medicine, Isfahan University of Medical Sciences, Isfahan, Iran. mry.moradi@gmail.com

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INTRODUCTION

While coronary artery stent implantation is a gold standard approach for coronary arteries stenosis causing angina and/or myocardial infarction, in-stent restenosis (ISR) is the main complication of this approach occurring in 20–35% of bare-metal stents and only 5–10% for drug-eluting stents.3-5

Coronary angiography is the standard approach for the assessment of ISR incidence and luminal stenosis severity that is an invasive procedure, posing considerable burden and costs in addition to its potential complications. Therefore, the requirement of a non-invasive means for ISR assessing is inevitably useful. Furthermore, gradual increase in number of patients undergoing coronary arteries stent placement better clarifies this requirement to minimize invasive procedures.6
ISR diagnosis is the most challenging matter among patients with coronary artery disease (CAD) undergone stenting. Although coronary computed tomography angiography (CCTA) has been widely utilized for coronary arteries assessing, its efficacy for stent evaluation due to artifacts of stent struts, especially beam hardening and its narrow lumen, is still an important issue.\(^1\)

Multidetector CT (MDCT) introduction made a great revolution regarding coronary stent assessment as it could provide high-quality images with satisfactory temporal and spatial resolution. Furthermore, there are limitations including the type of stent (bare metal/drug eluting) and its diameter, stent strut thickness, its angularity, and motional artifacts in quality of these images.\(^2,3,6,7\)

The last versions of CT scans have more rapid imaging reception, higher spatial and temporal resolution and have particular software capable of coronary arteries and stent reconstruction led to less biases. Furthermore, by cardiac rate control and breath holding during imaging, the motion artifacts have been minimized.\(^6\)

Nowadays, most of CCTA reports are based on visual assessing of contrast flow of stent lumen while this method does not have ideal diagnostic value with significant interobserver biases. Quantitative measurements provide more reliable information about the status of stents. Recent studies have presented variety of quantitative methods with acceptable sensitivity and specificity for the diagnosis of ISR.\(^6,10\)

The current study has aimed to provide a quantitative method for ISR estimation, in which predictive value of stent enhancement in CCTA would be evaluated.

MATERIALS AND METHODS

Study design and participants

This is a prospective cross-sectional study conducted on 40 patients with a history of coronary stent implantation that because of CAD symptoms, recurrence was referred for CCTA performance to MDCT scan center of Chamran Hospital affiliated at Isfahan University of Medical Sciences in 2017–2018.

Patients with CAD symptoms who had a previous history of stent implantation and have undergone conventional angiography during the 1st month following CCTA were included in the study.

Unavailability of conventional angiography images and patient's unwillingness of participation in the study were exclusion criteria.

All patients were asked about the presence of renal failure or any hypersensitivity to contrast agents. In addition, all of cardiovascular records of patients including their echocardiography were gathered to enter the required information in the study checklist. Then, patients who met inclusion criteria were prescribed sublingual nitroglycerine (0.4 mg, Dana; Iran) for vascular dilation and also oral beta-blocker to achieve appropriate rate control.

Test method

CCTA was performed using 256-slice MDCT scan (Brilliance TM 256; Philips Medical System) and specific workstation was utilized for their reports. The protocol of imaging was as follows:

The properties as collimation=96–128 mm, detector size=0.625 mm, rotation time=0.27 ms, voltage: 120 kv, and 180–200 mAs,

CCTA was primarily performed without contrast injection with an appropriate field of view to assess coronary arteries calcium score. Then, intravenous contrast (Visipaque 320 mg) with 70–90 cc volume, based on patients' height and weight, with 5–6 cc/s velocity and using bolus track method was injected. Finally, images were taken in prospective manner and the following reconstructions were sent to Philips workstation to provide CCTA reports.

Intraluminal enhancement of stent was measured by comparing calcium score and post-contrast images. In this regard, intraluminal density of stent was measured through focusing on the region of interest at the initial, middle, and end sites of stents in axial plane using calcium score images and repeat this measurement in post-contrast phase as well. The optimal post-contrast phase with less motion artifact and more resolution was considered for mentioned assessment. The difference between measured density presented by Hounsfield unit (HU) from similar sites derived before and after contrast injection was considered as intraluminal enhancement. To minimize interobserver bias, all of the measurements were performed by a target expert radiologist.

Analysis

Enhancement value (EV)=Post-contrast intraluminal density-calcium score intraluminal density.

Conventional invasive coronary angiography (CICA) was used as the gold standard and all patients CICA images reported only by a target cardiologist. CICA results were presented as patency, non-significant stenosis, and significant stenosis occluded. Due to clinical significance of stenosis, those with reports of patency and non-significant (<50%) were presented in a group and those with significant stenosis (over 50%) and occluded were presented in another group. These results were used for achieving cutoff point of EV in CCTA for differentiating these two groups of patients.
Obtained data were entered into SPSS-20 (IBM-The United States) software. ROC curve was drawn to demonstrate the cutoff point of EV for ISR prediction. In addition, sensitivity, specificity, positive predictive value (PPV), and negative predictive value (NPV) of stent enhancement were measured. $P < 0.05$ was considered as statistically significant level.

**RESULTS**

**Participants**

In the current study, a number of 40 patients with total number of 58 stents were assessed. A number of 15 (37.5%) of patients were female and remained 25 ones (62.5%) were male. The mean age of the study population was 60.97 ± 10.55 years old.

**Test results**

Characteristics of implanted stents are presented in Table 1. Twenty-eight out of 58 cases (41.4%) were implanted in the left anterior coronary artery, 10 (17.2%) in the left circumflex artery, and 16 (27.6%) in the right coronary artery. Nine of stents had <3 mm of diameter, 26 of them had 3 mm of diameter, and other 23 ones had over 3 mm diameter.

Among stents, 39 ones (67.24%) were patent or had ISR of <50%, 16 ones (29.31%) had over 50% stenosis, and 3 ones (3.44%) were completely occluded.

The cutoff point for EV was measured in three sites of stents in CCTA images that were achieved based on CICA findings. These cutoff points were 204, 168, and 204 HU for initial, middle, and end part of stents, respectively, which show more than 50% of ISR. Mentioned cutoff points are presented in Table 2. Considering no statistical difference among these cutoff points (use 168 or 204) ($P = 0.4$), 168 HU was considered as the most valuable cutoff for the diagnosis of over 50% ISR due to its higher sensitivity and PPV [Figure 1].

ISR was once measured based on stent intraluminal density just in post-contrast phase and then measured again using EV for comparison this method.

### Table 1: Characteristics of implanted stents.

| Parameter                  | Total | ISR <50% | ISR 50%–100% | ISR 100% |
|----------------------------|-------|----------|--------------|----------|
| Number of stents           | 58    | 39 (67.24%) | 16 (27.58%) | 3 (5.17%) |
| Location of stents         |       |          |              |          |
| Left anterior descending artery | 24 (41.4) | 15 (41.7) | 9 (56.3) | 0 |
| Left circumflex artery     | 10 (17.2) | 5 (13.9) | 2 (12.5) | 1 (33.3) |
| Right coronary artery      | 16 (27.6) | 12 (33.3) | 3 (18.8) | 1 (33.3) |
| Other                      | 8 (13.8) | 6 (11.1) | 2 (12.5) | 1 (33.3) |
| Stent diameter (mm)        |       |          |              |          |
| <3                         | 9 (15.5) | 7 (17.94) | 2 (12.5) | 0 |
| 3                          | 26 (44.8) | 20 (51.28) | 6 (37.5) | 0 |
| >3                         | 23 (39.6) | 12 (30.76) | 8 (50) | 3 (100) |
| Length (mm)                | 17.22±8.33* | 21.74±10.46* | 25.87±12.52* | 27.33±4.61* |
| Segment                    |       |          |              |          |
| Origin                     | 2 (3.4) | 1 (2.6) | 1 (6.3) | 0 |
| Proximal                   | 27 (46.6) | 21 (53.8) | 6 (37.5) | 0 |
| Proximal-middle            | 2 (3.4) | 1 (2.6) | 1 (6.3) | 0 |
| Middle                     | 23 (39.7) | 15 (38.5) | 7 (43.8) | 1 (33.3) |
| Middle-distal              | 1 (1.7) | 0 | 0 | 1 (33.3) |
| Distal                     | 3 (5.2) | 1 (2.6) | 1 (6.3) | 1 (33.3) |

*mean±SD

### Table 2: Sensitivity, specificity, positive predictive value, and likelihood ratio of EV and PCD for in-stent restenosis diagnosis.

| Index        | Cutoff point | Sensitivity (%) | Specificity (%) | Accuracy (%) | Likelihood ratio | AUC     | 95% CI    | $P$  |
|--------------|--------------|-----------------|-----------------|--------------|------------------|---------|-----------|------|
| PCD initial  | 500          | 79.49           | 63.16           | 74.14        | 2.15             | 0.69    | 0.53–0.85 | 0.404|
| EV initial   | 204          | 87              | 57.89           | 77.5         | 2.07             | 0.73    | 0.60–0.84 | 0.763|
| PCD mid      | 402          | 94.87           | 63.16           | 84.45        | 2.57             | 0.81    | 0.68–0.90 | 0.113|
| EV mid       | 168          | 92.3            | 73.68           | 86           | 3.5              | 0.85    | 0.68–0.90 | 0.113|
| PCD end      | 386          | 97.44           | 42              | 79.31        | 1.68             | 0.72    | 0.56–0.88 | 0.090|
| EV end       | 204          | 87              | 68              | 81           | 2.7              | 0.81    | 0.68–0.90 | 0.090|

EV: Enhancement value, PCD: Post-contrast density
Table 2 shows validity, specificity, PPV, and diagnostic value based on stent intraluminal EV and also based on stent intraluminal density in post-contrast phase for ISR diagnosis, mentioned as post-contrast density (PCD). Comparison of PPV of EV method versus PCD showed superiority of EV method.

Considering area under curve (AUC) of all three above figures, EV is superior to PCD regarding its better predictive value [Figure 2].

As stent diameter may have impact on intraluminal density, ISR diagnostic value in EV method was assessed before and after stent diameter adjustment. Maximal 4–7% of decrease in three points of initial, middle, and end part of stent AUC were found that was negligible.

**DISCUSSION**

Stent implantation is one of the old and effective treatments of coronary artery stenosis while ISR is among the most significant complications of this approach.\(^{[11,12]}\) Incidence of restenosis is in association with factors including the type of stent (metallic or drug eluting), stent diameter and length, and the individual's atherosclerotic factors such as diabetes.\(^{[3,4]}\) ISR diagnosis is made based on CICA. Although it is still the gold standard method of ISR diagnosis, its potential complications caused considerable trend toward non-invasive techniques.

Electron beam CT was the first non-invasive modality for stent status assessment introduced in 1995. In this method, it used images for flow-related analysis which showed flow limiting ISR indirectly. This method did not outlive due to its low spatial resolution, unavailability of direct stent lumen visualization, and inability for diagnosis non-obstructive intimal hyperplasia.\(^{[13]}\)

In the 1\(^{st}\) year of the 2000s, 4-slice CT scans were utilized, in which distal contrast runoff was the criterion of stent patency. These types of CTIs were eliminated as well due to its low spatial and temporal resolution. Moreover, this technique was also affected by collateral vessels. By 16-slice CT scans introduction, stent lumen observation was possible and new windows of non-invasive stent luminal status assessment were opened toward physicians.\(^{[2]}\) This superiority is while factors including type of stent, its strut thickness, luminal diameter, and angle and motional artifacts can affect new CT scan modalities efficacy in negative manner. New generations of CT scans (e.g., 64, 128, and 320 slice) provide higher number of cuts with less thickness obtained in fewer time and they have some software for coronary artery and stent reconstruction with specific filters such as sharp kernel, therefore, they can better visualize stent's lumen and provide more concise information about luminal status. Furthermore, new modalities provide reconstructed images with more clarified view of stents.\(^{[13,14]}\)

Qualitative stent patency assessment regarding intraluminal contrast flow has considerable interobserver bias, for narrow lumens in special. Quantitative method for luminal stenotic status estimation has better diagnostic values that have recently made them of great interest. In recent studies, various quantitative methods for ISR assessment such as corrected coronary opacification (CCO), remodeling index, lesion length, non-calcified lesion volume, and stent restenosis index (SRI) were introduced.\(^{[8-10]}\)
In most of quantitative methods mentioned above such as CCO introduced by Gao et al., in 2014,[9] or SRI presented by Yoshimura et al., in 2015,[10] coronary artery intraluminal density before and after stent was considered for patency assessment. Considering the fact that post-stent coronary artery intraluminal density would be affected by collateral vessels blood flow, direct stent luminal assessment seems superior.

SRI quantitative method was presented by Yoshimura et al., in which coronary artery intraluminal density before and after stent was measured and their difference based on luminal diameter correction was considered as stent stenotic status.[10] In the current study, we used EV method and presented our outcomes following pre- and post-stent diameter adjustment. Regarding ROC curve, diagnostic values were not considerably improved. Therefore, we concluded that stent diameter is negligible but further studies to assess the impact of stent diameter on EV assessment are recommended.

The other quantitative method introduced by Kitagawa et al. utilized intraluminal density difference of proximal to stent site with stent itself. They presented 70 HU as the reliable cutoff point for over 50% of ISR.[11]

Dr. Makoto Amanuma from Japan raised a novel method of ISR assessment, in which software for CT angiography subtraction has been used. The new method was accompanied with abilities including increased ISR diagnostic value and possibility of assessing stents with even <2.5 mm of diameter. In subtraction method, the final image will be achieved through comparison of images before and after contrast injection causing elimination of stent strut artifacts and calcified plaques. This superiority would be achieved in EV method introduced in our study as well.[12] Furthermore, EV method gives us qualitative information with easier manner.

Considering this fact that basis of the most of the previous recommended quantitative methods for stent assessment was performed in post-contrast phase and this phase may be affected by confounding factors such as stent strut blooming artifacts and its plaques, we have selected EV method which is achieved through comparison of with and without contrast phases. Therefore, the mentioned bias may be eliminated.

Furthermore, in the current study, post-contrast intraluminal HU for the assessment of ISR was compared with EV as well. Statistical comparison of two techniques in initial, middle, and end sites showed no statistical differences, while PPV of EV method was considerably superior to post-contrast phase.

Eventually, the current study achieved remarkable successful outcomes in assessing ISR, for lumens with <3 mm diameter in special, using 256-slice CT scan. This achievement occurred due to high velocity, better spatial and temporal resolution, and using specific reconstruction filters.

Limitations
Inaccessibility of data about the type of stent (stent brand) used for patients in their previous angiographic treatment is the most significant limitations of the current study.

Furthermore, we need larger sample volume for the evaluation of the effect of stent diameter and length and native coronary artery which contains stent on EV method.

CONCLUSION
The use of quantitative method of intraluminal stent enhancement for ISR estimation has better diagnostic value in comparison to qualitative and subjective methods that can help better clinical decision-making. Moreover, measurements of this method are somewhat easier and also secondary artifacts of stent strut and calcified plaques would be eliminated through EV method.

Declaration of patient consent
The authors certify that they have obtained all appropriate patient consent.

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Conflicts of interest
There are no conflicts of interest.

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