Effect of alginate concentration on chondrogenesis of co-cultured human adipose-derived stem cells and nasal chondrocytes: a biological study

Y. W. Ewa-Choy, B. Pingguan-Murphy, N. A. Abdul-Ghani, J. Jahendran and K. H. Chua

Abstract

**Background:** The three-dimensional (3D) system is one of the important factors to engineer a biocompatible and functional scaffold for the applications of cell-based therapies for cartilage repair. The 3D alginate hydrogels system has previously been shown to potentially promote chondrogenesis. The chondrocytic differentiation of co-cultured adipose-derived stem cells (ADSCs) and nasal chondrocytes (NCs) within alginate constructs are hypothesized to be influenced by concentration of alginate hydrogel. In this study, we evaluated the effects of alginate concentration on chondrogenic differentiation of ADSCs and NCs co-cultured in a biological approach.

**Method:** The co-cultured cells of 2:1 ADSCs-to-NCs ratio were encapsulated in alginate constructs in one of three concentrations (1.0%, 1.2% and 1.5%) and cultured under serum free conditions for 7 days. Cell viability, cell proliferation, immunohistochemical, gycosaminoglycans (GAG) synthesis, and gene expression were examined.

**Results:** Overall, the 1.2% alginate concentration group was relatively effective in chondrocytic differentiation in comparable to other groups. The cell morphology, cell viability, and cell proliferation revealed initial chondrogenic differentiation by the formation of cell clusters as well as the high permeability for exchange of solutes. The formation of newly synthesis cartilage-specific extracellular matrix in 1.2% group was demonstrated by positive immunohistochemical staining of collagen type II. The co-cultured cells in 1.2% group highly expressed COL II, ACP and SOX-9, compared to 1.0% and 1.5% groups, denote the retention of cartilaginous-specific phenotype by suppressing the undifferentiation stem cell markers of SOX-2 and OCT-4. The study showed 1.2% group was less likely to differentiate towards osteogenesis by downregulating hyperthrophy chondrocytic gene of COL X and osseous marker genes of OSC and OSP.

**Conclusion:** This study suggests that variations in the alginate concentration of co-cultured ADSCs and NCs influenced the chondrogenesis. The remarkable biological performance on chondrogenic differentiation in regulating the concentration of alginate 3D culture provides new insights into the cell cross-talk and demonstrates the effectiveness in regenerative therapies of cartilage defects in tissue engineering.

**Keywords:** Alginate concentration, Chondrogenesis, Co-cultured, Human adipose-derived stem cells, Nasal chondrocytes, Three-dimensional system, Cartilage repair

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Background
Injectable alginate hydrogels system has recently raised the interest in tissue engineering and regenerative medicine. The challenges such as the invasive implantation procedure and poor cell retention within the defect can be improved using this system [1–3]. The injectable delivery system allows cells encapsulated in hydrogels to exactly fill tissue voids and complex defects in the articular surface [4]. The three-dimensional (3D) system plays a crucial role leading to a successful injectable alginate hydrogels system with the recent advancement of cell-based tissue engineering application in cartilage regeneration. Culturing cells in 3D environment is well known for cell cross-talk and cell-to-extracellular matrix (ECM) interactions for initial chondrocytic differentiation and maintain of chondrogenic phenotype [5]. 3D culture mimics the in vivo microenvironment to promote strong cellular interactions. Recent studies demonstrated superior chondrogenesis by co-culturing mesenchymal stem cells (MSCs) and articular chondrocytes in 3D culture environment than monolayer culture [6–8]. However, the co-cultured cells in 3D microenvironment with direct cellular interactions has the tendency to form heterokaryons [9].

The 3D alginate hydrogels system has been proposed to physically immobilize the co-cultured cells via minimal direct cell contact [10]. Alginate has been extensively used as a biocompatible carrier for cartilaginous regeneration in tissue engineering approaches. Encapsulation of cells in alginate is capable to crosslink with calcium to form hydrogels and function at the physiological conditions. The alginate properties of natural hydrocolloidal in gelation tend to form a stable quasi-solid structure with high porosity and water content. The pore structure is highly dependent on the concentration of hydrogel. Theoretically the increase in concentration of hydrogels may reduce in efficiency of solutes transportation and nutrient supply and therefore, leading to a lower diffusion coefficient [11]. Several studies indicated the transport of solutes is concentration dependence, which the diffusion coefficient decreased with higher concentration of alginate gel [12, 13].

To date, there are very few studies on the co-cultured system using alginate constructs as the biomaterial for cartilaginous regeneration in cell-based tissue engineering. A comparative study evaluated the chondrogenic differentiation potential of a single cell type supplemented with growth factors [14]. Some reports focused mainly on the mechanical properties of alginate constructs with or without cells [15–17]. However, there are no quantitative and systematic study especially on the concentration of alginate hydrogels as a scaffold material to drive chondrogenesis of MSCs in a co-culture model on a biological approach. Cell sources remained as one of the factors that are pivotal to the success of chondrocytic differentiation via co-culture system. Adipose-derived stem cells (ADSCs) are widely known to be an attractive alternative source of adult stem cells which is capable of self-renewal and proliferate in a large degree with its high telomerase activity [18, 19], while nasal septum cartilage or nasal chondrocytes (NCs) serve as a great alternative source of non-articular cartilage that eliminated the issue of donor morbidity and still preserve the chondrocytic phenotype [20]. ADSCs culture in alginate hydrogels have previously been proven to promote chondrogenic differentiation [21, 22]. The chondrogenic differentiation of ADSCs can be increased with appropriate ratio of chondrocytes in co-culture and the cell seeding density [23]. However, another crucial issue for ADSCs chondrogenesis in alginate hydrogels is the gel concentration because it affects the complex interaction of growth and differentiation factors as well as nutrient and waste flow. Therefore, the interest raised on the study to determine the most effective concentration of alginate hydrogel to provide the appropriate physiological conditions of microenvironment for chondrogenic differentiation by co-culturing ADSCs and NCs. In this study, the biological performance on the efficacy of alginate hydrogel concentration on chondrocytic differentiation with encapsulation of co-cultured ADSCs and NCs have been investigated.

Methods
Harvesting and expansion of human adipose-derived stem cells (ADSCs)
The human abdominal subcutaneous adipose tissues were harvested from patients (n = 6, where n is sample size) with written informed consent after caesarean section and all the experimental procedures were approved by the Research Ethics Committee Universiti Kebangsaan Malaysia (FF-2015-220). The adipose tissue was minced into small pieces. These pieces were then digested with 0.3% collagenase type 1 (Worthington Biochemical Corporation, NJ, USA) for an hour in an orbital shaker incubator at 37 °C. The supernatant was aspirated and the tissue was washed twice with phosphate-buffered saline (PBS; pH 7.22, Gibco, NY, USA). The isolated ADSCs were resuspended in complete medium (Ham’s F12 and Dulbecco’s modified Eagle medium (DMEM/F-12; Gibco) containing 10% fetal bovine serum (FBS; Gibco), 1% antibiotic-antimycotic (Gibco), 1% glutamax (Gibco), and 1% of 50 μg/ml ascorbic acid (Sigma-Aldrich, St. Louis, USA)) and incubated in vitro to confluence. The medium was changed every 48 h. The cells were trypsinized using 0.125% trypsin-ethylene diamine tetra acetic acid (EDTA; Gibco) and subcultured until passage 3 to 5 for encapsulation in alginate constructs.
Harvesting and expansion of human nasal Chondrocytes (NCs)
The nasal septum cartilage was harvested from six patients ($n = 6$) who underwent an elective septoplasty procedure with written informed consent (approved by Research Ethics Committee Universiti Kebangsaan Malaysia with approval ethic code, FF-2015-220). The septal cartilage specimen was diced into fine pieces. The diced cartilage were digested using 0.6% collagenase type II (Worthington Biochemical Corporation, NJ, USA) in an orbital shaker incubator for 4 h at 37 °C. The supernatant was discarded and the cell pellet was washed with PBS. The isolated NCs were cultured in complete medium (as described in harvesting and expansion of ADSCs) and incubated at 5% CO$_2$ at 37 °C. The medium was changed every other day. The cells were trypsinized using 0.125% trypsin-EDTA and then proceeded with encapsulation for chondrogenic differentiation.

Alginate encapsulation of co-culture ADSCs and NCs
The powder form of sodium alginate (Sigma-Aldrich, USA) was weighed accordingly and dissolved in 0.9% w/v sodium chloride solution to form aqueous solution with the concentrations of 1.0%, 1.2%, and 1.5%. Three million cells comprising of ADSCs and NCs were co-cultured in 2:1 ratio. The cell ratio of 2:1 was the optimum co-culture ratio as previously determined to promote chondrogenesis [23]. The mixture of cells were resuspended in alginate solution to a final cell density of $3 \times 10^6$ cells/ml and the final alginate concentrations respectively as previously described [24, 25]. The suspension was pressed through a syringe with 27-gauge needle in a droplet method into the 102 mM calcium chloride solution that initiated gelation and formed spherical alginate-cell constructs. The alginate-cell constructs were maintained for 8 min in 102 mM calcium chloride solution to complete the polymerization process. The constructs were then filtered using cell strainer and were rinsed with 0.9% sodium chloride solution and serum free medium (Ham’s F12 and Dulbecco’s modified Eagle medium (DMEM/F-12; Gibco) supplemented with 1% Insulin-Transferring-Selenium-X Supplement (ITS; Gibco), 1% antibiotic-antimycotic, 1% glutamax, and 1% ascorbic acid) successively. The microencapsulated cells were cultured in suspension cultures for 7 days with serum free medium. The medium was replaced every alternate day.

Morphological assessment and cell viability
The alginate-cell constructs were observed with an imaging system (EVOS FL Colour; Life Technologies, USA) and the morphology of encapsulated cells were photographed at day 7. The viability of the co-cultured cells in the alginate hydrogel was evaluated with trypan blue exclusion test using a haemocytometer.

Immunohistochemical analysis
After 7 days in culture, the constructs were fixed in 10% formalin and embedded into paraffin. Sections with a thickness of 5 μm were cut. The presence of collagen type II was immunolocalized with mouse monoclonal antibody against collagen type II (Thermo Scientific, USA). After 30 min of room temperature incubation with primary antibody, sections were incubated with rabbit anti-mouse secondary antibody (DAKO, Denmark) for another 30 min. This is followed by positive staining visualization using 3,3’-Diaminobenzidine (DAB; DAKO) and counterstained nucleus in hemotoxylin. Microscopic images were photographed with a microscopy imaging system (Q550IW; Leica, Germany).

Cell proliferation
Deoxyribonucleic acid (DNA) content of microencapsulated cells was quantified at day 7 for cell proliferation assessment. The samples were purified using PureLink Genomic DNA mini kit (Life Technologies, USA). Total DNA of digested sample was quantified using UV-Vis spectrophotometer (NanoDrop 2000; Thermo Scientific, USA).

Biochemical analysis
Glycosaminoglycan (GAG) is the major component of cartilage extracellular matrix. After 7 days of culture, the synthesis of GAG was evaluated by the 1,9-dimethylmethylenylene blue (DMMB; Biocolor, UK) method. The samples were digested in papain lysis buffer (Sigma-Aldrich, USA) for 3 h at 65 °C. The amount of GAG accumulation in alginate-cell construct was tabulated by calibrating against a standard curve constructed from bovine tracheal chondroitin-4-sulfate (Biocolor, UK). The absorbance was detected using a microplate spectrophotometer (Thermo Scientific, USA) at a wavelength of 595 nm. The GAG content was normalized to the DNA content to examine the biosynthetic activity of microencapsulated cells.

RNA extraction and gene expression
Real-time polymerase chain reaction (RT-PCR) was used to quantify the expression of targeted genes in each sample at day 7. The samples were digested using TRIzol reagent (Invitrogen, USA) and the total RNA were extracted. Total RNA was transcribed into single-strand cDNA using SuperScript III First-strand synthesis kit (Life technologies, USA) in accordance to manufacturer’s recommendations. Table 1 shows the genes for RT-PCR analysis: chondrogenic genes were used as positive gene expressions, stemness genes were served as negative control, and osteogenic genes were used to regulate osteogenesis. All targeted genes were normalized to the endogenous housekeeping gene, Glyceraldehyde-3-phosphate dehydrogenase (GAPDH). The PCR reaction
was evaluated using the SYBR Select Master Mix (Life technologies, USA) with a RT-PCR machine (iCycler; Bio-Rad, USA). The effects of cartilaginous phenotype restoration were analyzed using COL II-to-COL I ratio.

**Table 1** List of primer sequences for RT-PCR analysis

| Gene                                | Primer 5' - 3'                                      | Accession no. |
|-------------------------------------|--------------------------------------------------|---------------|
| GADPH                               | F: 5'-ccc ttc aac tgc tga aag cga aag cat ctc-3'   | NM_002046     |
|                                     | R: 5'-gaa gaa gta gtt ggt gtt gtc gct gc-3'       |               |
| Human Collagen                      | F: 5'-agg gct cca aag aca tca agg gag atg gaa-3'  | NM_000886     |
| Type I, COL I                       | R: 5'-tac aag cag aca gaa gaa gga tgt ctc agc-3'  |               |
| Human Collagen                      | F: 5'-cta tct gaa cga aag aca tgg gc-3'           | NM_001844     |
| Type II, COL II                     | R: 5'-tct gtt ctc ttc agc tca gtg cgc-3'          |               |
| Human Aggrecan                      | F: 5'-cac tgt tac cgc cac ttc cc-3'                | NM_001135     |
| Core Protein, ACP                   | R: 5'-acc aac gga agt ccc ctt gcg-3'              |               |
| Human Transcription Factor SOX-9    | F: 5'-gcg gag gaa gtc ggt gaa gaa-3'              | NM_000346     |
| SOX-9                               | R: 5'-ccc tct cgc ttc agg tca gc-3'               |               |
| Homeobox Transcription Factor, NANOG | F: 5'-ctg tga ttt gtt ggc ctg aa-3'              | NM_024865     |
|                                      | R: 5'-tct gtt ccc tgt gga ctt gc-3'               |               |
| SRY-related                         | F: 5'-taa ctt ctt cct ccc act cca-3'              | NM_003106     |
| HMG-Box-2, SOX-2                    | R: 5'-ggg atg gct ggg atc taa gaa-3'              |               |
| Reduced Expression-1, REX-1         | F: 5'-aaa ggt ttt cga aag aag ctc-3'              | NM_174900     |
|                                      | R: 5'-ctg cga gct gtt tag gat cgg-3'              |               |
| Octamer-Binding Protein 3/4, OCT-4  | F: 5'-aag gat gtt gtc cga gtt gtt cgc cgg gaa-3' | NM_002701     |
|                                      | R: 5'-gaa gtt agg gct ccc ata gc-3'               |               |
| Osteocalcin                          | F: 5'-gtg cag aat cca aag ggt gaa gt-3'           | NM_199173     |
| OCT-4                               | R: 5'-tga gcc aac tgg tca cag ctc-3'              |               |
| Osteopontin, OSP                    | F: 5'-tga aac gag gta gtt gga gaa gga-3'          | NM_001040060  |
|                                      | R: 5'-ttg tgg tcg tgg tgg gta aa-3'              |               |
| Human Collagen                      | F: 5'-gtc aac gaa gag agt ctt cgg ctt cca gcc-3'  | NM_000493     |
| Type X, COL X                       | R: 5'-ctc cag gat cac ctt ctt gta ga-3'           |               |

**Results**

**Cell viability**

The microscopic images (Fig. 1a-c) illustrated the plump and rounded morphology of co-cultured ADSCs and NCs encapsulated in alginate constructs with various concentrations. The size of alginate constructs remained spherical shape in all groups during a cultivation period of 7 days (Fig. 1d-f). The cells were sparsely and evenly distributed throughout the transparent matrix constructs. Cell clusters were found in all constructs with various concentrations, especially for the condition with the higher alginate concentrations of 1.2% and 1.5%, in which the number of cell clusters was greater. The cell viability of ADSCs and NCs with coculture ratio 2:1 in alginate construct were significant higher in 1.5% group and followed by 1.0% and 1.2% groups at day 7 (Fig. 2). All alginate concentration groups maintained high viability rate, ranging from 66% to 72% in which the differences were relatively narrow.

**Production of cartilaginous extracellular matrix**

The presence of collagen type II was detected by immunohistochemical staining. Positive staining for collagen type II was observed with all alginate concentration groups (Fig. 3). Sections were stained on single cells and small cell clusters. Consistent with cell morphological assessment, the cells encapsulated in alginate constructs were exhibited in round shape and were slightly more intensely aggregated in 1.2% and 1.5% of alginate concentration groups. The formation of lacunae revealed the synthesis of ECM was largely observed in 1.2% group compared to other groups.

**Production of DNA and GAG contents**

The DNA content indicated the proliferation rate of cocultured ADSCs and NCs encapsulated in alginate constructs with increasing concentrations. The amount of DNA was significantly higher in alginate concentration of 1.5% group comparable to other groups after cultured for 7 days, whereas 1.0% group has a lower cellularity and followed by 1.2% group (Fig. 4a). This cell proliferation data was responded to the cell viability rate, in which an increase in cell viability with the highest alginate concentration group. The amount of GAG content was quantified by DMMA assay throughout cultivation period of 7 days. The newly synthesis GAG contents of 1.5% alginate concentration group has a significant increase compared to other lower alginate concentration groups (Fig. 4b). The finding of GAG synthesis was in agreed with the amount of DNA content.
The amount of GAG content was normalized to amount of DNA content (Fig. 4c) to demonstrate differences in the biosynthesis activity of the co-cultured cells among the groups with various alginate concentrations. The normalization of GAG/DNA revealed similar trends in all groups, however there was no significant differences after normalization in each group.

**Gene expression analysis**

The co-cultured of ADSCs and NCs were encapsulated in alginate constructs with different alginate concentrations were analyzed. The alginate concentration of 1.2% group demonstrated an overall remarkable upregulation of chondrogenic marker genes in comparison to 1.5% concentration group at day 7 (Fig. 5b-d). The 1.2% group showed a nearly 300-fold induction of ACP expression. The cartilaginous markers of SOX-9 was highly expressed in 1.2% group and showed a significant increase by 516-fold respectively. Conversely, the expression of stemness gene markers was strongly downregulated in 1.2% alginate concentration group. The gene expression of NANOG, SOX-2, REX-1 AND OCT-4 were significantly higher in 1.5% group after cultured for 7 days, whereas 1.0% group maintained at a lower level in all stemness markers (Fig. 5e-h). The osteogenic markers of OSC, OSP and COL X were analyzed to evaluate the osteogenesis.

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**Fig. 1** Morphological appearance of various concentrations of alginate constructs encapsulated with co-cultured ADSCs and NCs. a Study group with 1.0% of alginate concentration under magnification of 20x. b Study group with 1.2% of alginate concentration under magnification of 20x. c Study group with 1.5% of alginate concentration under magnification of 20x. d Study group with 1.0% of alginate concentration under magnification of 5x. e Study group with 1.2% of alginate concentration under magnification of 5x. f Study group with 1.5% of alginate concentration under magnification of 5x.

**Fig. 2** The cell viability of alginate constructs with different concentrations after 7 days of culture.
tendency of co-cultured ADSCs and NCs in alginate constructs. The co-cultured cells in 1.2% alginate concentration group showed a low level of expression in osteogenic genes (Fig. 5i-k). However, the 1.0% and 1.5% groups significantly upregulated OSP and COL X at day 7.

COL II was normalized to COL I to analyze the restoration index of cartilaginous phenotype among different alginate concentration groups as showed in Fig. 6. The COL II-to-COL I ratio demonstrated the significant differences in 1.2% group in relative to 1.0% and 1.5% groups.

**Discussion**

Recent studies reported alginate is an established and biocompatible hydrogel scaffold material that is capable for cartilaginous regeneration [16, 26]. However, there is no quantitative biological study on the effects of alginate concentration in chondrogenic differentiation of co-cultured system. Also, current commercially available cellular based therapy required a long cultivation period to prepare sufficient amount of chondrocytes for transplantation [27, 28]. Thus, our study aimed to develop early chondrogenic progenitor cells achieved by 3D alginate co-cultured system to shorten the culture period when comes to clinical application. In this study, we evaluated the efficacy of chondrogenic pre-differentiation when encapsulated co-cultured ADSCs and NCs in the ratio of 2:1 in alginate constructs with different concentrations. All the study groups were evaluated at day 7 as previous study shown that cells showed evident of chondrogenesis as early as 7 days by forming dense spherical cellular bodies with the setting [29].

The ADSCs and NCs exhibited a spherical morphology when co-cultured in the three-dimensional alginate hydrogels even in serum free culture condition. The co-cultured cells encapsulated in alginate constructs underwent an instant chondrogenic switch to recover their cartilaginous-specific phenotype [30, 31]. The co-cultured cell aggregates and formed cell clusters at day 7 demonstrated the formation of early chondrogenic differentiation especially in 1.2% and 1.5% groups. Previous studies reported the formation of functional tissue-engineered cartilage tissue initiated with the formation of cellular aggregates as early as cultivation period of 5 days [29, 32]. The cell viability in alginate constructs with various concentrations was relatively high after cultivation period of 7 days. The high percentage of viable cells indicated the high permeability of the alginate constructs that allows
adequate amount of nutrient supply to the cells even in the serum free cultured condition. The cross-linking of alginate-cells by calcium creates a highly hydrated three-dimensional microenvironment at physiological conditions, in which the cells encapsulated in alginate constructs are highly functional and have a high cellularity [33].

The cartilage-specific extracellular matrix (ECM) of collagen type II was deposited within the alginate constructs among different concentration of alginate groups from immunohistochemical analysis. The production of ECM is relatively high by alginate concentration of 1.2% group with the observation of lacunae synthesis. The

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**Fig. 4** DNA and GAG content in alginate constructs with different concentrations were quantified respectively. **a** Amount of DNA content. **b** Synthesis of GAG. **c** Normalization of GAG content to DNA content
Fig. 5 Quantitative real-time gene expressions analysis of a-d chondrogenic genes, e-h stemness genes, and i-k osteogenic genes. a COL I, b COL II, c ACP, d SOX-9, e NANOG, f SOX-2, g REX-1, h OCT-4, i OSC, j OSP, k COL X.

Fig. 6 Quantitative analysis of cartilaginous phenotype restoration index of COL II-to-COL I.
results were consistent with the morphological assessment, in which the aggregation of cells and formation of cell clusters were observed the demonstration of cartilaginous matrix to form early chondrogenesis.

In this study, the amount of DNA denotes the quantitative analysis of cell proliferation. Since the cells were immobilized in the alginate constructs, we would not expect significant increase in cell proliferation [25, 34]. Consistent with the findings in this study, the overall amount of DNA in each study group is within the moderate range. However, we did note that the lower DNA content in 1.2% group had much higher viability of cells, which is consistent as the previous findings [26]. The GAG content exhibited a similar trend which lower amount of cartilaginous matrix was observed in 1.2% group than other groups. This is possibly due to the encapsulated co-cultured cells are in the initial stage of cellular condensation process in 1.2% alginate constructs [14]. The normalization of GAG-to-DNA showed significant differences in 1.2% group which demonstrates the biosynthesis activities were initiated at this concentration compared to other concentration groups. Although 1.0% and 1.5% groups exhibited higher cell proliferation and GAG content, the gene expressions in both study groups demonstrated a low level of chondrogenic gene expression.

The quantitative analysis of real-time PCR was used to study the gene expressions patterns in various concentrations of alginate constructs. The co-cultured of ADSCs and NCs showed an expression of chondrocyte-specific marker genes such as ACP, SOX-9, collagen type II and collagen type I. With regard to alginate concentration, the 1.2% group expressed high level of the chondrogenic genes, whereas other groups remained low level of expressions. The higher expression of ACP represent the newly synthesis of cartilaginous ECM [35, 36]. The early markers for chondrogenesis such as COL I serve as the most abundant collagen in human body [37] and SOX-9 act as a transcription factor to regulate the other gene expression involved in chondrogenic differentiation [38]. In contrast, the stemness markers were highly upregulated in 1.5% group comparable to the significantly downregulated 1.2% group, which denotes the co-cultured cells in 1.5% group preserve most of the stemness properties such as NANOG and REX-1 impose the pluripotency on stem cells and remained undifferentiated [39]. SOX-2 is the transcription regulators that forms a trimeric complex with OCT-4 to regulate the number of stemness gene expressions [40], while OCT-4 is commonly used as an undifferentiated stem cells marker due to the self-renewal ability of undifferentiated stem cells [41]. To exclude the unwanted osteogenic differentiation of the cultured cells, OSC and OSP was analyzed. The expression of osseous marker genes were decreased significantly in 1.2% group compared to 1.5% group, whereas 1.0% group exhibited higher osteogenic markers as well. OSC is one of the osteoblast specific gene and OSP is responsible for bone mineralization [42, 43]. This suggests higher GAG content in 1.0% group has the tendency moving towards osteogenesis. The promotion of Collagen type X indicates hypertrophic chondrocytes that may led the co-cultured cells to eventually differentiated towards osteogenesis [44]. Downregulated of COL X in 1.2% group compared to 1.5% group indicates minimal hypertrophy as COL X is not favorable in ECM of hyaline cartilage [45]. The overall quantitative mRNA expression profile suggests the alginate concentration of 1.2% group yielded the most favourable chondrogenic differentiation when encapsulated with co-cultured ADSCs and NCs by maintaining the healthy chondrocytic phenotype without the tendency to differentiate into bone.

This study demonstrated the 1.5% group exhibited higher synthesis of ECM, however the gene expression shows that higher stemness properties are also found within this group, in which suggesting most of the ADSCs were remained undifferentiated and the high matrix production may secrete mainly by NCs than ADSCs.

The properties of alginate constructs are dependent on the process of cross-linking. The concentration of alginate solution is one of the factor which influence the stiffness or elasticity of the alginate constructs after gelation [33]. The current study suggests the lowest alginate concentration of 1.0% was too lowand the highest alginate concentration of 1.5% was quite stiff to induce proper chondrocytic differentiation when compared to 1.2% group. The alginate constructs having an optimum concentration of 1.2% resulted from the cartilage-like cell morphology, high cell viability, synthesis of new ECM, and upregulation of chondrogenic marker genes, give rise to a stiffer and more stable hydrogel scaffold biomaterial. It has been studied in the recent literature that the gold standard of cartilage regeneration therapeutic approaches for encapsulation of cell culture in alginate hydrogel is 1.2%, in which support the findings of the current study [46, 47].

Conclusion

In summary, these findings are quite evident that the variations in concentrations of alginate constructs by co-culturing ADSCs and NCs influences the cartilaginous differentiation. Our data suggests alginate constructs in different concentrations create a microenvironment that influenced the chondrocytic differentiation with support of cell viability and gene expressions. This study contributes to better understanding of the effects of alginate concentration in the aspect of stem cell differentiation, suggesting the potential application in cartilage tissue engineering.
Abbreviations
3D : Three-Dimensional; ACP: Human AggreCan Core Protein; ADSCs: Adipose-Derived Stem Cells; COL I: Human Collagen Type I; COL II: Human Collagen Type II; COL X: Human Collagen Type X; DAB: 3,3'-Diaminobenzidine; DMEF/F-12: Ham's F12 and Dulbecco's Modified Eagle Medium; DMEM: 1,9-Dimethylmethylenedioxy Blue; DNA: Deoxyribonucleic Acid; ECM: Extracellular Matrix; EDTA: Tris(hydroxymethyl)aminomethane; FBS: Fetal Bovine Serum; GAG: Gycosaminoglycans; GAPDH: Glucose-6-phosphate Dehydrogenase; ITS: Insulin-Transferring-Selenium-X; MSCs: Mesenchymal Stem Cells; NanoDG: Homeobox Transcription Factor; NCs: Nasal Chondrocytes; OCT-4: Octamer-Binding Protein 3/4; OSC: Osteocalcin; OSF: Osteostrin; PBS: Phosphate-Buffered Saline; PETS: Phosphatase-Buffered Saline; RT-PCR: Real-Time Polymerase Chain Reaction; SOX-2: SRY-related HMG-Box-2; SOX-9: Human Transcription Factor SOX-9

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Availability of data and materials
All data generated or analysed during this study are included in this published article.

Authors' contributions
YWEC: Study design, conduct experiment, preparation of manuscript. BPM: Study design, preparation of manuscript. NAAG: Study design, sample preparation. JJ: Study design, sample preparation. YHCH: Study design, preparation of manuscript, corresponding author. All authors read and approved the final manuscript.

Ethics approval and consent to participate
Human abdominal subcutaneous adipose tissues were collected from patients with written informed consent after caesarean section performed at Universiti Kebangsaan Malaysia Medical Centre (Approved by Research Ethics Committee Universiti Kebangsaan Malaysia with approval code, FF-2015-220). Cartilage specimens were harvested from the human nasal septum of the patients who underwent an elective septoplasty procedure with written informed consent (approved by Research Ethics Committee Universiti Kebangsaan Malaysia with approval ethic code, FF-2015-220).

Consent for publication
Not applicable.

Competing interests
The authors declare that they have no competing interests.

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