Perceptual Space of Algorithms for Three-to-One Dimensional Reduction of Realistic Vibrations

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Abstract—Haptics researchers often endeavor to deliver realistic vibrotactile feedback through broad-bandwidth actuators; however, these actuators typically generate only single-axis vibrations, not 3D vibrations like those that occur in natural tool-mediated interactions. Several three-to-one (321) dimensional reduction algorithms have thus been developed to combine 3D vibrations into 1D vibrations. Surprisingly, the perceptual quality of 321-converted vibrations has never been comprehensively compared to rendering of the original 3D signals. In this study, we develop a multi-dimensional vibration rendering system using a magnetic levitation haptic interface. We verify the system’s ability to generate realistic 3D vibrations recorded in both tapping and dragging interactions with four surfaces. We then conduct a study with 15 participants to measure the perceived dissimilarities between five 321 algorithms (SAZ, SUM, VM, DFT, PCA) and the original recordings. The resulting perceptual space is investigated with multiple regression and Procrustes analysis to unveil the relationship between the physical and perceptual properties of 321-converted vibrations. Surprisingly, we found that participants perceptually discriminated the original 3D vibrations from all tested 1D versions. Overall, our results indicate that spectral, temporal, and directional attributes may all contribute to the perceived similarities of vibration signals.

Index Terms—Magnetic levitation haptic interface, vibrotactile rendering, perceptual space, dimensional reduction algorithm.

I. INTRODUCTION

Physical interactions between real objects generate vibrations that help humans perceive material properties and textures. Tool-mediated contacts evoke particularly strong vibrations because a stiff object experiences many transients when making and breaking contact. By providing vibrotactile feedback in computer-mediated applications, recent haptic displays take advantage of the human sensitivity to vibrations and thereby enrich user interactions [1]. Software developers synthesize or pattern artificial vibration models to alert the user to important events or provide context-sensitive information [2]. Applications developed for virtual reality [3], [4] and robotic teleoperation [5], [6] often seek to deliver realistic vibrotactile cues similar to those felt in real interactions.

Natural vibrations from tool-mediated interactions are generally three-dimensional (3D) and contain energy at a broad range of frequencies [5], [7]. To mimic natural interactions in virtual environments, developers usually implement realistic vibrotactile feedback using either a physics-based model designed by hapticians or a data-driven model established from vibratory signals recorded in real environments [8]. However, in practice, rendering realistic vibrations via typical haptic devices and actuators is more challenging than computing the signal to be rendered. Many force-feedback devices do not excel at rendering high-frequency vibrations [9], [10] due to the friction, flexibility, and mechanical backlash that their mechanisms contain. These characteristics somewhat limit the controllability of the device [11]. Therefore, commercial vibration actuators that can output arbitrary broad-bandwidth waveforms are often used to display realistic vibrotactile cues [1]; many such devices are electromagnetic and function similar to small audio speakers. However, these actuators generate vibrations along only one fixed axis, so they cannot immediately output a 3D vibration that has been synthesized or recorded. Although three such actuators can be combined to create 3D vibrations, the system’s cost, complexity, weight, inertia, and volume all increase; a single actuator is more practical.

To render realistic vibrations using 1D vibration actuators, several haptics researchers have been looking for an effective method to convert 3D vibrations to 1D vibrations, called a three-to-one (321) dimensional reduction algorithm [12]. The belief that such a conversion exists somewhat stems from the fact that a Pacinian corpuscle (PC, the main mechanoreceptor that senses high-frequency mechanical vibrations in human skin) is less sensitive to the direction of stimuli than other mechanoreceptors [13], [14]. The ideal 321 algorithm would preserve all useful information when converting 3D vibrations into 1D so that the resulting signal feels indistinguishable...
from the original version. Various 321 algorithms have been developed and tested, from the simplest approach that keeps only a single axis aligned with the main interaction direction, e.g., [15], to more computationally intensive options such as DFT321 [12], which leverages the discrete Fourier transform.

Previously, Park and Kuchenbecker investigated the effectiveness of 321 algorithms via performance metrics and a perceptual study [16]. Their users touched various surfaces with a pen-shaped sensing tool, while a one-axis actuating tool displayed a dimensionally reduced version of the measured three-axis vibration to the other hand in real time. The users rated the perceptual similarity between the vibrations felt on the two tools for each algorithm and surface. Although some of the tested 321 algorithms generated 1D vibrations that felt reasonably similar to the original 3D vibrations, most received comparable scores, and none matched exceptionally well.

For a more detailed performance examination, this paper aims to characterize the shared perceptual space of the original 3D and converted 1D vibrations produced by common 321 algorithms. Many studies have used the perceptual space approach [17] for haptics because this tool adeptly showcases the similarities and differences in human perception of complex stimuli. Such a comparison requires a haptic interface that can render multi-dimensional vibratory feedback effectively. One feasible way to create such vibrations uses magnetic levitation; the frictionless, stiff, and backlash-free transmission of such devices gives them the potential to produce high-frequency vibrations [18]. Recently, Zhang et al. used an untethered stylus-like magnetic levitation device constructed from large coils and a small permanent magnet to render 1D vibrations along/around each of the 6D translational and rotational axes [19]. They investigated 1D vibration detection thresholds for each axis as well as the effects of the physical parameters of the stylus for a precision grasping posture [20]. Furthermore, they used perceptual results gathered with this device to propose a six-to-one (621) dimensional reduction matrix that can effectively convert 6D vibrations into 1D at a single frequency (108 Hz) [21] or at a range of frequencies from 20 to 250 Hz [22].

Similar to the approach of Zhang et al. [21], this paper introduces a multi-dimensional vibration rendering system built around magnetic actuation. After careful characterization, this system can provide realistic vibration feedback, playing broad-bandwidth vibrations simultaneously along multiple axes. The paper then presents our findings from the user study, establishing the perceptual space of 321 algorithms for realistic vibrations rendered by the proposed system.

II. MULTI-DIMENSIONAL VIBRATION RENDERING SYSTEM

A. Hardware

We used a commercial magnetic levitation haptic interface (Maglev 200, Butterfly Haptics LLC) [23] to create a multi-dimensional vibration rendering system (Fig. 1). The interface can render continuous 6-DoF wrench feedback \( \mathbf{W} = [F_x, F_y, F_z, \tau_x, \tau_y, \tau_z]^T \) (see coordinate frame in Fig. 1(a)) with zero friction and no mechanical backlash. This device’s simple and joint-free mechanical design enables it to consistently output high-frequency vibration signals. The peak force and force resolution of the device are 40 N and 20 mN, respectively. After testing various servo rates and wrench commanding rates, we set both to 1 kHz to keep the delay small and constant. As a result, according to the Nyquist-Shannon sampling theorem, the system can produce continuous vibrations in a frequency range up to 500 Hz. Although it does not fully cover the sensitivity of PCs (approximately 20–1000 Hz), it covers a broad range that impedance-type haptic devices with multi-joint structures may not easily produce [24].

We considered the common situation where a user holds a stylus with a precision grip and feels a cutaneous vibration caused by a surface interaction at the lower end of the stylus [Fig. 1(b)]. To this end, we custom-designed and attached a stylus-like rigid manipulandum (11.5 cm, \( \varnothing = 6 \text{ mm} \), assembled from a 10-cm aluminum cylinder-shaped rod and a copper base) to the top of the device end-effector. The weight of the manipulandum (450 g) is light enough to be compensated by the software. An accelerometer (ADXL354, Analog Devices) is rigidly mounted inside the manipulandum to record 3D acceleration signals aligned to the translational axes of \( x, y, \) and \( z \). A data acquisition board (USB-6343, National Instruments) is used to record the stylus’ three-axis acceleration data at a sampling rate of 10 kHz.

B. Dynamic Compensation

To render high-fidelity realistic vibration signals, one must characterize the transfer function (TF) of the rendering device from force/torque to acceleration and compensate for its dynamics [25]. We can approximately cancel the dynamics of the system by applying an inverse TF (ITF) filter to the desired acceleration signal to calculate the command [26]. When this model adequately captures the dominant dynamics, we can expect the device output to be similar to the desired acceleration waveform.

The user grasps about 6 cm above the accelerometer located inside of the manipulandum. We observe that five different sources in the 6-DoF wrench (\( \mathbf{W} \)) can independently contribute to the creation of each axial component of the 3D acceleration vector \( \mathbf{a} = [a_x, a_y, a_z]^T \) measured by the accelerometer. First, the 3-DoF force components (\( F_x, F_y, \) and \( F_z \)) mainly produce accelerations aligned with their respective axes (\( a_z, \)
\(a_x\), and \(a_y\). Second, high-frequency torques around the \(x\) axis \((\tau_x)\) mainly generate stylus accelerations along \(y\) \((a_y)\), just as torques around the \(y\) axis \((\tau_y)\) mainly cause accelerations along \(x\) \((a_x)\). To limit the complexity of our model, we fit a single-input single-output (SISO) system with five independent TFs: \(H_{F_x}, H_{F_y}, H_{F_z}, H_{y} \) (for \(a_x\)), and \(H_{y} \) (for \(a_y\)), using the following data-driven procedure [27].

First, we command a 30-s, 10–500-Hz linear swept sinusoid for each condition (three trials for \(F_x\) and \(F_y\), ten for \(F_z\), and five for \(\tau_x\) and \(\tau_y\)) to provide some variety in hand posture and torques around the \(x\) axis. By applying \(\tilde{H}^{-1}(\omega)\), we can transform each original acceleration command into a measurable impact on the resulting transfer functions. However, changing the dynamic model according to each individual or hand posture would be inefficient in terms of data collection, model fitting, and device use. Instead, we chose the simple and practical solution of carefully fitting one dynamic model to a single individual’s varied dataset and employing it for all users.

The selected participant conducted multiple measurement trials for each condition (three trials for \(F_x\) and \(F_y\), ten for \(F_z\), and five for \(\tau_x\) and \(\tau_y\)) to provide some variety in hand posture and to allow us to confirm that the data were repeatable. Then, based on the relationship between sweep input and output in each trial, we obtain a trial-wise frequency response of the system and its inverse form. For example, from a 1-N sweep input \(F_x(t)\) and its measured output acceleration \(a_{x,i}(t)\) in the \(i\)-th measurement trial, \(H_{i}(\omega) = \mathcal{F}(a_{x,i}(t))/\mathcal{F}(F_x(t))\) and \(H_{i}^{-1}(\omega) = \mathcal{F}(a_{x,i}(t))/\mathcal{F}(F_x(t))\) between \(\omega_{\text{min}} = 20\pi\) rad/s (10 Hz) and \(\omega_{\text{max}} = 1000\pi\) rad/s (500 Hz) are computed.

Next, a nonparametric ITF model \(\tilde{H}^{-1}(\omega)\) was obtained by smoothing all trial-wise frequency responses using an empirical TF estimate (ETF) [28].

The planar force-based filters \((H_{F_x} \text{ and } H_{F_y})\) contain sharp peaks below 100 Hz [Fig. 2(a) and (b)]. When we apply these models to a vibration containing low-frequency components, the resulting force command may exceed the device limit. Therefore, to keep the commands within the device’s capabilities, we selected ITF filters as torque-based models for \(x\) and \(y\) \((H_{\tau_x} \text{ and } H_{\tau_y})\) and a force-based model for \(z\) \((H_{F_z})\).

![Figure 2](image-url)

**Fig. 2.** ITF models for dynamic compensation. Blue dotted lines are trial-wise measurements. Black bold lines are smoothed nonparametric models, red dashed lines show continuous models, and green dotted lines show the final discrete models. (a) \(H_{F_x}^{-1} \cdot \mathcal{F}(F_x)\). (b) \(H_{F_y}^{-1} \cdot \mathcal{F}(F_y)\). (c) \(H_{F_z}^{-1} \cdot \mathcal{F}(F_z)\). (d) \(H_{\tau_x}^{-1} \cdot \mathcal{F}(\tau_x)\). (e) \(H_{\tau_y}^{-1} \cdot \mathcal{F}(\tau_y)\).

\[
\tilde{H}^{-1}(s) = e^{-\xi s} \frac{Z(s)}{P(s)},
\]

where the polynomials of \(P(s)\) and \(Z(s)\) are its poles and zeros, respectively. \(\xi\) is a time delay. \(\tilde{H}^{-1}(s)\) was established by testing different numbers of poles and zeros to find the smallest error between \(\tilde{H}^{-1}(\omega)\) and \(\tilde{H}^{-1}(s)\). Then, we discretized \(\tilde{H}^{-1}(s)\) to get a discrete-time model \(\tilde{H}^{-1}(z)\) using the matched pole–zero (MPZ) transform, i.e., \(z = e^{s}\Delta t\) [29].

\[\Delta t = 0.1\ \text{ms}\] is a time interval of the accelerometer’s sampling rate (10 kHz). An identical ITF filter \(\tilde{H}^{-1}(\omega)\) can be implemented from the same poles and zeros of \(\tilde{H}^{-1}(z)\).

\(C.\) **Results**

We conducted the characterization process via MATLAB (2019a, The MathWorks). The Bode plots of the five resulting ITF models in the frequency range of interest are presented in Fig. 2. We estimated the fitting accuracy using the root mean squared error (RMSE) and the normalized RMSE (NRMSE) between the empirical nonparametric model \((\tilde{H})\) and the resulting parameterized model \((\tilde{H}^{-1})\), each calculated as follows:

\[
\text{RMSE} = \sqrt{\frac{1}{\omega_{\text{max}} - \omega_{\text{min}}} \sum_{\omega = \omega_{\text{min}}}^{\omega_{\text{max}}} \left( |\tilde{H}^{-1}(\omega)| - |\tilde{H}^{-1}(\omega)| \right)^2},
\]

\[
\text{NRMSE} = \frac{1}{\omega_{\text{max}} - \omega_{\text{min}}} \sum_{\omega = \omega_{\text{min}}}^{\omega_{\text{max}}} \left( \frac{|\tilde{H}^{-1}(\omega)| - |\tilde{H}^{-1}(\omega)|}{|\tilde{H}^{-1}(\omega)|} \right)^2.
\]

Table I presents the order and fitting accuracy of each ITF model. All achieved a fitting accuracy over 90%, which is expected to sufficiently cancel out the dynamics of the system.
D. Crosstalk Analysis

If the system does not follow our SISO assumption, its rendering performance will be poor due to interference across axes. We thus analyzed the undesired mechanical vibrations generated in the directions orthogonal to the desired axis (so-called crosstalk) for each considered force and torque input. Using the recorded sweep data and the same ETFE procedure, we obtained 15 different smoothed forward TFs, $H_{W_s}^{\omega}(\omega)$, each describing the relationship from a single input force/torque command $W_s \in \{F_x, F_y, F_z, \tau_x, \tau_y\}$ in $W$ to one of the single output accelerations $a_s \in \{a_x, a_y, a_z\}$ in 3D.

The relative crosstalk $R_{i,j}^a$ was then quantified as the ratio of the sum of the magnitude spectrum of $H_{W_s}^{\omega}$ on the target non-dominant axis to the sum of the magnitude spectrum of $H_{W_s}^{\omega}$ on its dominant axis, within our target frequency range from $\omega_{\text{min}}$ to $\omega_{\text{max}}$, as follows:

$$R_{i,j}^a = \frac{\sum_{\omega=\omega_{\text{min}}}^{\omega_{\text{max}}} |H_{W_s}^{\omega,i}(\omega)|}{\sum_{\omega=\omega_{\text{min}}}^{\omega_{\text{max}}} |H_{W_s}^{\omega,j}(\omega)|},$$

where $a_D$ represents the acceleration along the dominant axis for $W_s$ (e.g., $a_D = a_x$ for both $F_x$ and $\tau_y$). Table II shows the resulting values: the crosstalk generated by each actuation source is much smaller than the vibration the same command causes on its dominant axis (always less than 16%), thereby justifying our SISO assumption. The results further showcase that $R_{F_x}^{a_x}$ and $R_{F_z}^{a_z}$ are about two times larger than $R_{F_y}^{a_y}$ and $R_{\tau_x}^{a_z}$. This finding that torque commands cause less crosstalk than comparable force commands reinforces our decision to use torques to render lateral accelerations with this haptic device.

III. DATA ACQUISITION

We recorded a set of real three-axis vibration signals, $a(t) = [a_x(t) \ a_y(t) \ a_z(t)]^T$. Fig. 3(a) demonstrates the data collection procedure. The accelerometer, the data acquisition board, the shape of the stylus, the hand posture, and the grasping position on the stylus were all the same as in Section II-A.

Similar to [16], we selected four surfaces (100 mm × 100 mm) to provide different hardness and roughness sensations during a stylus-based interaction. The tiles are made of sandpaper, acrylic, rough paper, and rubber, and each material represents the tactile sensation of hard/rough (HR), hard/smooth (HS), soft/rough (SR), and soft/smooth (SS), respectively (Fig. 3(b)).

In [16], the experimenter interacted with each surface with a composite movement, tapping its surface three times and then dragging the stylus in a circle three times. In contrast, we separated tapping and dragging because each move generates accelerations mainly in a different direction. In our tapping recordings (denoted as T), the experimenter hits perpendicular to the surface five times with the instrumented stylus [Fig. 3(c)]. Since tapping is a 1D movement along the surface normal, this interaction results in a series of impulse-like vibrations mainly along the $z$ direction. In dragging (denoted as D), the experimenter moves the stylus along the surface in an inverted-L-shaped stroke, once along the $x$-axis followed by once along the $y$-axis [Fig. 3(d)]. Dragging the stylus generates a vivid 3D vibration that depends on the geometry and material properties of both the tool tip and the surface; most of the signal energy is in the direction of travel and perpendicular to the surface.

We collected a total of eight interactions with the two different movements and four surfaces: THR, THS, TSR, TSS, DHR, DHS, DSR, and DSS. By repeating each measurement four times, we obtained a collection of 32 acceleration-based vibrations. During each interaction, a video was recorded simultaneously with sound using a standard webcam; see the examples of these recordings in part 1 (tapping) and part 2 (dragging) of the supplementary video. All of the collected vibration data and the corresponding videos can be found on IEEE DataPort [30].

To output vibrations, we command a wrench $W_{in} = [0 \ 0 \ F_z \ \tau_y \ \tau_x \ 0]$ to the system, where $W_{in}$ is obtained by applying the selected ITF filters to the corresponding input acceleration $a_{in}$ after application of a 20–500 Hz band-pass filter. The experimenter held the stylus and recorded the corresponding output signal $a_{out}$ during each execution. Fig. 4 illustrates input-output examples in situations that are somewhat challenging to render: tapping on a hard/smooth surface (THS) and dragging on a soft/rough surface (DSR). These examples

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**TABLE I**

| $n(P)$ | $H_{P_1}^{\omega}$ | $H_{P_2}^{\omega}$ | $H_{P_3}^{\omega}$ | $H_{P_4}^{\omega}$ | $H_{P_5}^{\omega}$ |
|--------|--------------------|--------------------|--------------------|--------------------|--------------------|
| 6      | 9                  | 1                  | 11                 | 12                 | 6                  |
| 9      | 1                  | 5                  | 13                 | 12                 | 10                 |

**TABLE II**

| Axis | $R_{F_x}^{a_x}$ | $R_{F_y}^{a_y}$ | $R_{F_z}^{a_z}$ | $R_{\tau_x}^{a_z}$ | $R_{\tau_y}^{a_z}$ |
|------|----------------|----------------|----------------|-------------------|-------------------|
| $a_x$| (100%)         | 10.50%         | 2.80%          | 6.96%             | (100%)           |
| $a_y$| 15.49%         | (100%)         | 3.37%          | (100%)            | 6.07%             |
| $a_z$| 1.97%          | 3.17%          | (100%)         | 3.06%             | 2.16%             |

**Fig. 3.** Data acquisition of realistic vibrations using a combination of two movements and four surface materials. (a) The recording device assembled from a stylus and an accelerometer. (b) The four surfaces. (c) The tapping movement on acrylic. (d) The dragging movement on sandpaper.
This method is x;y;z a P 1 ^ and utilizes the DFT to can be used. We extract by f e largely match in both time and fre-

\[
A_i(t) = \mathcal{F}\{a_i(t)\} = |A_i(f)|e^{i\Theta_i(f)},
\]

where |A_i(f)| and \(\Theta_i(f)\) denote the spectral magnitude and the phase information, respectively. The algorithm then synthesizes three frequency components into \(\hat{A}(f) = |\hat{A}(f)|e^{i\hat{\Theta}(f)}\), where
\[ w = \text{PCA}(M), \]
\[ \hat{a}(t) = w^T a(t), \]

where \( \text{PCA}(M) \) finds a unit vector along the principal axis of the distribution in a data matrix \( M \), which is composed of the acceleration vector \( a \) over time. This algorithm is similar to \( \text{SAZ} \), except the chosen axis depends on the signal itself. Windowed time segments \( \hat{a}(t) \) can be leveraged to respond to directional changes over short time intervals [16]. For consistency, the same window used in \( \text{DFT} \) was used for \( \text{PCA} \).

**B. Spectral and Temporal Matching Metrics**

To quantitatively compare the performance of 321 algorithms, Landin et al. first introduced a spectral matching score and a time matching score, which compare the original 3D signal \( a(t) \) and the reduced 1D signal \( \hat{a}(t) \) in the frequency and time domains [12]. Adopting the same idea, several researchers have developed or improved similar metrics to assess the quality of vibrotactile signals [16], [31].

**Spectral Matching** \( (M_{sm}) \) computes the spectral similarity between the original 3D signal and the reduced 1D signal \( a \). We use Park and Kuchenbecker’s enhanced version of this metric, incorporating the perceptual characteristics of differential thresholds (DLs) of vibration frequencies [16]. First, the signals are normalized as

\[ N(a(t)) = \frac{a(t)}{a_{\max}}, \quad (10) \]

\[ N(\hat{a}(t)) = \frac{\hat{a}(t)}{\hat{a}_{\max}}, \quad (11) \]

where \( a_{\max} = \max(|a(t)|) \). We then obtain the normalized frequency spectra \( \{N A_i(f) = F\{a_i(t)\}\} \) \( i \in \{x,y,z\} \) and \( N A(f) = F(\hat{a}(t)) \) using \( \text{DFT} \).

We then decompose the entire frequency range \( f_{\min} = 20 \) Hz to \( f_{\max} = 500 \) Hz into \( n \) different intervals \( \{f : f_n \leq f < f_{n+1}\} \), updating \( f_n \) as

\[ f_{n+1} = \begin{cases} 1.1 f_n, & \text{if } 1.1 f_n < f_{\max}, \\ f_{\max}, & \text{otherwise}, \end{cases} \quad (12) \]

until \( f_{n+1} \) reaches \( f_{\max} \). Equation (12) is inspired by the perceptual property that a frequency increased by 10% from the reference frequency is still below the DL at moderate vibration magnitudes of 20 dB sensation level (dB SL) [32]. The dissimilarity value \( d_n \) is computed for each interval as

\[ d_n = \frac{\sum_{f \in F_n} \left( |N A(f)|^2 - |N \hat{A}(f)|^2 \right)}{\sum_{f \in F_n} |N A(f)|^2}, \quad (13) \]

where \( |N A(f)|^2 = \sum_{i \in \{x,y,z\}} |N A_i(f)|^2 \). We then average all \( d_n \)'s to compute the mean spectral difference \( D \) between the original and reduced signals.

The decomposition process weighs different human sensitivities according to different frequencies. However, when the frequency resolution is not precise, such \( d_n \)'s depend on each individual value of the frequency components in the spectrum (especially at low frequencies); this causes an unexpected distortion of the actual values [16]. To prevent this side-effect, we acquire the spectral differences \( D_{20} \) and \( D_{21} \), each of which starts from different frequencies, \( f_1 = f_{\min} = 20 \) Hz or \( f_1 = 21 \) Hz (purposefully separated by halving the initial DL), respectively. Finally, we compute \( M_{sm} \) as

\[ M_{sm} = \begin{cases} 1 - D, & \text{if } D < 1, \\ 0, & \text{otherwise}. \end{cases} \quad (14) \]

where the smoothed value \( D = \frac{1}{2} (D_{20} + D_{21}) \). Negative values are changed to zero to limit the score to the 0–1 range.

**Temporal Matching** \( (M_{tm}) \) computes the temporal similarity between the original and reduced signals. \( M_{tm} \) is computed as

\[ M_{tm} = \frac{1}{3} \sum_{x,y,z} \left| \frac{|N a_i(t) \ast N \hat{a}(t)|}{|N a_i(t) \ast N \hat{a}(t)| + |N a_i(t) \ast N \hat{a}(t)| + |N a_i(t) \ast N \hat{a}(t)|} \right|, \quad (15) \]

where the operator \( \ast \) denotes the cross-correlation of two signals evaluated at zero time delay. Equation (15) averages the absolute values of the normalized cross-correlations (in the 0–1 range) across the three axes.

**C. Objective Evaluation**

Before investigating the perceptual space of these 321 methods, we evaluated their objective performance with both matching metrics. Using our multi-dimensional rendering system, we rendered 160 vibrations (32 recorded 3D acceleration signals converted to 1D by the five algorithms) along the \( z \) axis and measured the acceleration while a user held the stylus.

Fig. 5 depicts the means of \( M_{sm} \) and \( M_{tm} \) between the input and output accelerations, averaged across the four different measurements for each interaction. The input and the rendered output had similar matching scores, again showcasing the high fidelity of our rendering approach. These objective scores are ratio-scaled data; therefore, to study the effects of surface material and 321 algorithm, we performed a parametric test of two-way analysis of variance (ANOVA) on each of the four datasets (\( M_{sm} \) or \( M_{tm} \) for tapping or dragging). Every analysis reported that both main effects and their interaction were statistically significant at \( \alpha = 0.05 \) (\( p < 0.05 \)).

For more detailed post-hoc analysis, we additionally conducted Tukey’s HSD test (Fig. 5). We found that most of our results were consistent with the previous studies of 321 algorithms ([12] and [16]). The overall ranking of \( M_{tm} \) in tapping, which mainly occurs along the \( z \) axis, was \( \text{DFT} \geq \text{PCA} \geq \text{SAZ} \geq \text{SUM} \geq \text{VM} \), where the highest is best. VM consistently showed the lowest \( M_{sm} \), followed by SUM. DFT showed the highest score, which indicates that the normalized frequency spectrum of DFT was the most similar to the original 3D signal. In dragging interactions, the overall ranking of \( M_{sm} \) was \( \text{DFT} \approx \text{PCA} \geq \text{SUM} \geq \text{VM} \geq \text{SAZ} \text{SAZ} \), which is limited to display only the vibrations orthogonal to the surface, showed a considerable limitation in the presentation of spectral information in dragging. DFT and PCA were similarly rated as the highest in
contending with each other to be the best matching algorithm over all types of surface material. In both tapping and dragging, the overall ranking of $M_{sm}$ scores varied significantly depending on the surface texture type, because most methods showed similar scores. VM consistently achieved the lowest score for $M_{sm}$.

In summary, the spectral similarity between dimensionally reduced acceleration signals and the original signal is different from method to method. DFT or PCA showed the best score in both interactions; thus, these methods can be expected to be the best dimensional reduction methods to keep the spectral characteristics of the original 3D signal. VM was found to be the worst method for spectral match in tapping and temporal match in dragging. All other evaluated dimensional reduction algorithms show a similar capability to maintain the temporal properties of the original signal. Their scores are lower in dragging interactions than tapping interactions, meaning that the algorithms may lose more temporal information when applied to rich 3D signals compared to mainly 1D signals.

V. PERCEPTUAL EXPERIMENT

We conducted an experiment to compare the cutaneous perception of vibrotactile stimuli created by different 321 algorithms. All vibration signals were rendered by the multi-dimensional system using dynamic compensation.

A. Participants

A total of fifteen participants (six males and nine females; 11 right-handed and four left-handed; 24–41 years old, M: 31.3, SD: 5.6) participated in this experiment. The location of the haptic device was rearranged before the experiment so each participant could use their dominant hand comfortably. All participants reported no visual, auditory, or sensory-motor disabilities. This experiment was approved by the Ethics Council of the Max Planck Society under the Haptic Intelligence Department’s framework agreement (F010A). All participants signed a consent document after being informed about the procedure. Participants not employed by the Max Planck Society were compensated 20 EUR (8 EUR per hour).

B. Stimuli

Our recorded dataset of real vibrations ([30]; see Section III) includes four examples for each surface interaction. From each set, we selected the example whose renderings best showed the trend of the average $M_{sm}$ across the five algorithms in Section IV-C. Each representative recording was converted to six different experimental stimuli, including the original 3D vibration (ORI) and 1D vibrations dimensionally reduced by the five 321 algorithms (SAZ, SUM, VM, DFT, PCA). All 1D vibrations were displayed using only the $z$-axis, which is aligned with the stylus. The resulting set of 48 wrench commands (4 surfaces $\times$ 2 interactions $\times$ 6 algorithms) was used in the study.

C. Procedure

Participants were seated in front of the system in a comfortable posture and instructed to stretch their dominant hand to grasp the stylus with a precision grip (Fig. 6). The view of their hand and the haptic device was blocked by a curtain. They also wore noise-isolating headphones during the experiment to block auditory cues from the device and other noise sources. During the experiment, the experimenter monitored the participant and corrected their hand posture if it changed in order to minimize the trial-wise variations in the system dynamics. Each block of the study featured one interaction and consisted of a pair of consecutive sessions. The first session in the pair
was a practice session to let participants accustom themselves to all of the stimuli. Thus, only the responses in the second session were used for the analysis. The order of the eight featured interactions was randomized. Each session contained 15 comparison trials to compare each pair of the six algorithms. The order of the stimuli was also randomized.

In each trial, the participant was presented with two 5-s vibration stimuli and was instructed to rate their pairwise dissimilarity. Each vibration was mapped onto either the A or B buttons on a graphical interface. After a participant clicked either A or B using the mouse with the non-dominant hand, the corresponding vibration was played on the device. In synchrony with the rendered vibration, the associated video recording was displayed in a separate pop-up window, and the sound recording was simultaneously played on the headphones. The A and B buttons were disabled after being clicked so that the participant could feel each vibration only once.

We followed the general protocol of absolute magnitude estimation (on a free scale without a standard stimulus or a modulus) [33]. After feeling both stimuli, the participant was asked to enter a non-negative dissimilarity score for the two experienced stimuli, using the number keypad with the non-dominant hand. The participant was instructed to enter zero if the two stimuli felt identical. The comparison procedure is shown in part 3 of the supplementary video. A participant could proceed to the next trial or session by clicking the Next button. Previous responses could be changed by clicking the Previous button, but the other buttons remained disabled to prevent the participant from feeling the previous stimuli again.

After completing two consecutive sessions for the same condition, a participant was asked to take a break for at least one minute to prevent fatigue and sensory adaptation. A participant could take additional breaks between sessions. It took about 7.5 minutes to finish each session. Thus, the whole experiment was completed in two and a half hours.

D. Data Analysis

Since humans tend to use absolute scales rather than ratio scales for judging stimuli, this absolute magnitude estimation protocol avoids the contextual effects of natural human biases [34]. We first normalized the dissimilarity scores of each participant to a 0–100 scale using his or her maximum dissimilarity rating across all test trials to minimize individual differences that might exist. Then, the normalized dissimilarity scores in each interaction type were averaged across the participants and formatted into a dissimilarity matrix. These absolute dissimilarity values ensure ratio-scaled psychophysical data [35], rather than the ordinal or interval scales used in ordinary human response tests [36]. Therefore, we used each dissimilarity matrix as the input to a metric multi-dimensional scaling (MDS) to establish a corresponding perceptual space. During the computation of MDS, we assessed the goodness-of-fit of every dimension using Kruskal’s stress values. The stress value ranges from 0–1, and smaller indicates a better fit. A detailed procedure for MDS can be found in [37].

Although perceptual spaces implicitly visualize the relationship between stimuli, the axes generally do not coincide with any dimensions that are meaningful for interpretation [38]. Therefore, further investigation is usually conducted by analyzing additional ratings using subjective measures [39]. The most common approach is discovering semantic information related to perception by using adjectives as descriptors [40], [41]. In contrast, some studies have applied physical properties directly as descriptors to find systematic relationships between physical and perceptual properties because the responses to construct perceptual spaces are based on the apparent physical properties in tactile stimuli [36], [42].

Similarly, we aim to determine which characteristics of dimensional reduction algorithms can lead to perceived discrepancies. Therefore, we adopt several ratings related to the physical quality of vibrations to clarify the relationship between perceptual and physical spaces. First, we computed the matching scores \(M_{sm}\) and \(M_{tm}\), which show the spectral and temporal similarity to the original vibrations for all stimuli used in the experiment. \(M_{sm} = 1\) and \(M_{tm} = 1\) were assumed for ORI. Second, we consider the energy (or power) of the vibration signal transmitted to the skin mechanoreceptors as another major factor in recognition of perceived differences [36]. We calculated the signal energy \(E\) for each vibration:

\[
E = \sum_{f \in F} \sum_{i \in \{x, y, z\}} |A_i(f)|^2,
\]

where \(F\) is the frequency range that can be rendered and transmitted to the participant by our rendering system (20–500 Hz). Then, we applied multiple linear regression analysis with all 2D positions in each perceptual space as independent variables, using \(M_{sm}\), \(M_{tm}\), or \(E\) as dependent variables.

Lastly, to generalize and illustrate the perceptual relationship between 321 algorithms more clearly, we applied Procrustes analysis to bridge perceptual and physical properties. The Procrustes analysis primarily aims to map two representations onto each other as closely as possible by using only linear transformations (translation, scaling, reflection, and rotation, which are valid operations because the perceptual space yields only relative positions of percepts) [43], [44]. Therefore, the optimal transformation matrix to fit the points in a particular shape can
be suggested by the analysis. As mentioned before, most perceptual spaces show a relationship close to orthogonal between the two $M_{sm}$ and $M_{tm}$ axes. Hence, we fitted each perceptual MDS output to each physical space of $M_{sm}$ and $M_{tm}$ scores by linearly transforming them using a Procrustes function in MATLAB. This Procrustes transformation into the combined physical-perceptual space strongly preserves the relative locations of points in the perceptual space and provides additional information about their tendencies along the $M_{sm}$ axis and the $M_{tm}$ axis. Because this transformation is a linear approximation, the stimuli may be shown at locations that are different from their original two-dimensional locations in the $M_{sm}$-$M_{tm}$ plane. The Procrustes function also outputs a goodness-of-fit value that calculates the sum of squared errors between the original points and the fitted points, where lower values are better.

E. Results and Discussion

There exists a trade-off between the difficulty of the visualization in perceptual spaces and the accuracy of the MDS result. Therefore, stress values lower than 0.15 are commonly recommended for the goodness-of-fit [45]. For a 2D representation, we achieved stress values of 0.125 (THR), 0.109 (THS), 0.101 (TSR), 0.148 (TSS), 0.073 (DHR), 0.058 (DHS), 0.088 (DSS), and 0.070 (DSS). These low stress values indicate that two dimensions sufficiently capture the relationships among all stimuli; 2D visualizations are also beneficially easy to understand. We plot a total of eight different 2D perceptual spaces (denoted as $P_X$ for the surface interaction $X$) individually in Fig. 7.

The Euclidean distance between two stimuli shows the average perceived difference between that pair of corresponding vibrations, i.e., the perceived difference between those two 321 algorithms. Thus, one can discover some meaningful insights by analyzing pairwise distances.

First, we computed and summarized the distances from every 321 algorithm to ORI in Table III. This metric simply reveals the perceived difference from each stimulus to the original 3D vibration. Most of the perceptual spaces showed a distance between ORI and all 1D vibrations that is larger than the distances between the 1D vibrations, particularly in the dragging conditions, which involve 3D signals. The average distance also appears larger in the interactions with rough textures than with smooth ones. In the tapping condition, the overall ranking of mean distances between ORI and each dimensional reduction algorithm across four different textures was $DFT > VM > SAZ > PCA > SUM$. However, this ranking hardly matches with the ranking for each surface type. While $SUM$ or $PCA$ was located closest to ORI in three perceptual spaces ($P_{THR}$, $P_{THS}$, and $P_{TSS}$), SAZ was the nearest in $P_{TSS}$. In the dragging condition, the overall ranking of mean distances between ORI and each algorithm was $SAZ > VM > PCA > SUM > DFT$. Unlike the tapping conditions, this result was consistent with the individual rankings; $DFT$ or $SUM$ was located closest or second closest to ORI. $DFT$ was usually located slightly closer to ORI than $PCA$ (except $P_{DSS}$), whereas $SUM$ showed a similar distance to ORI with $DFT$ and $PCA$ but had more variation across surfaces. In all dragging conditions, $SAZ$ and $VM$ had the most and the second most different perception from ORI, respectively.

Second, we computed and summarized the distances between $SAZ$ and all other stimuli in Table IV because the displacement...
of SAZ from the other 1D vibrations is one observable factor shown differently in the perceptual spaces between tapping and dragging. For tapping, the overall ranking of average distances from SAZ was VM > SUM > PCA > DFT, and this ranking is more prominently shown in the conditions involving hard surfaces (THR and THS). In dragging interactions, the perceptual differences between SAZ and other algorithms were greater than in tapping interactions, and these differences became even larger on rougher surfaces (DHR and DSR). The overall ranking of the means of this distance metric was consistent as DFT > (PCA or SUM) > VM across surfaces. Therefore, DFT was perceived as most different from SAZ, whereas VM was perceived the most similar to SAZ.

We depicted potential descriptive axes acquired by the multiple linear regression analysis in every perceptual space in Fig. 7. The standardized regression coefficients were used to represent the slope of each axis. Table V summarizes the detailed statistical analysis for $M_{sm}$ and $E$ in the perceptual spaces.

![Table III](https://example.com/table3.png)

![Table IV](https://example.com/table4.png)

![Table V](https://example.com/table5.png)

The results showed that the relative 2D positions of stimuli arranged in the perceptual spaces are closely related to the $M_{sm}$ score or the signal energy $E$, with high $R^2$ values and significant $p$-values. In three perceptual spaces for tapping ($P_{THS}$, $P_{TSR}$, and $P_{TSS}$), $M_{sm}$ was the most descriptive with the highest correlation with the spatial arrangement of the stimuli. $E$ was the most significant metric only in $P_{THR}$. Both $M_{sm}$ and $E$ were also effective at explaining the distribution of positions in most of the dragging perceptual spaces, except $P_{DHR}$, which achieved marginal significance. $M_{sm}$ also showed a correlation to the relative positions to explain some relationship in most of the perceptual spaces, particularly in the perceptual spaces involving hard surfaces ($P_{THR}$, $P_{THS}$, $P_{DHR}$, and $P_{DHS}$). $P_{TSS}$ was the only perceptual space for a soft-surface interaction that was highly correlated to $M_{sm}$. The results indicate that the perceptual differences and the physical (spectral and temporal) differences between algorithms are correlated with each other to some extent.

The $M_{sm}$ axis (spectral similarity) and the $E$ axis (overall spectral energy) were often close to parallel, indicating a strong correlation. On the other hand, the two axes of $M_{sm}$ and $M_{sm}$ (temporal similarity) were closer to orthogonal in most perceptual spaces, which implies a complementary relationship. Except for $P_{TSR}$, most perceptual spaces showed similar trends, and the perceptual spaces associated with dragging showed them more clearly. We further investigated the exceptional condition TSR and found that this is the only condition where the signal energy $E$ of SUM (0.70 m$^2$/s$^3$) becomes unusually larger than that of ORI (0.43 m$^2$/s$^3$). This case is a particular example that reveals the weakness of SUM in maintaining the total energy, which means that generalization is more difficult than with other methods.

The perceptual spaces mapped to the $M_{sm}$-$M_{sm}$-physical matching parameters (later called physical-perceptual spaces) and their Procrustes values (low enough to show a reasonable fit) are presented in Fig. 8. Each group of four physical-perceptual spaces for the two featured interactions (tapping and dragging) shows a similar horizontal-vertical alignment of elements, regardless of the surface type. Almost every physical-perceptual space shows that the perceptual difference between 1D vibration and 3D vibration is greater than the differences between various 321-converted vibrations. This finding means that the participants were able to sense a discrepancy between the original 3D vibration and all 321-converted 1D vibrations regardless of which algorithm had been applied and which surface or interaction was featured.

VI. General Discussion

A. Comparison With Prior Perceptual Results

In [16], Park and Kuchenbecker assessed the same five algorithms by measuring the subjective similarity between the
original haptic interaction and its real-time-converted 1D vibration from participants’ responses on a Likert scale from 1 to 7. Several interpretations can be inferred from this previous study: first, the similarity scores of dimensionally reduced vibrations were about 4.8, implying that participants could tell the difference between the original 3D interaction (which included low-frequency contact forces) and the reduced 1D vibrations. Second, the overall variance of the similarity scores was relatively smaller than that of the physical similarity scores, showing that physical dissimilarities and perceptual dissimilarities are not in simple proportionality. Third, although every algorithm was rated well, **DFT** seemed to provide a slightly better feel, i.e., a more similar perception to the original 3D vibration, than others, particularly during interactions with rough surfaces. Interestingly, **SUM** often achieved a perceptual similarity comparable to **DFT**. Since this method has lower computational cost and induces no time delay, it may be a good option for real-time implementation.

Our study presents the same implications as [16] with additional interpretation in more detail. In most of the spaces in Fig. 8, the 321-converted vibrations were distributed along the horizontal direction, seemingly parallel to the $M_m$ axis. Moreover, **SAZ** and **DFT** were placed farthest apart as the leftmost and rightmost algorithms in those spaces for dragging, following their low and high $M_m$ scores, respectively. The vibration in tapping mainly occurs along the $z$-axis, which is the principal axis of the movement. Conversely, the vibration in dragging always occurs both along the movement direction (in 2D, both $x$ and $y$) and along the $z$-axis, resulting in a relatively even distribution to all three axes. In these regards, the low $M_m$ score of **SAZ** in dragging reflects that its spectrum includes only one axis. Furthermore, **DFT** can be regarded as the best algorithm for dragging because this method has the highest $M_m$ score and results in the closest (rightmost) perception to the original 3D vibration. These results imply that matching the spectral information contributes to the perceptual similarity, especially for rich signals with broad spectral components. On the other hand, our physical-perceptual spaces for both tapping and dragging consistently show a vertical gap between the 1D vibrations and the 3D vibration, similar to Park and Kuchenbecker’s finding that none of the tested algorithms earned an average similarity score higher than 5 out of 7 [16].

**B. Factors Contributing to Perceptual Dissimilarity**

What information allowed the participants to differentiate the reduced 1D vibrations from the original 3D vibrations? Since it is aligned with the $M_m$ axis in our analyses and the 1D vibrations all earned relatively low scores, it is tempting to attribute this difference to poor temporal matching. However, this gap could also originate from other differences that exist between these stimulus sets. It is not yet known what information is most important and how humans use it when making perceptual judgments. Therefore, we discuss some clues that participants might have used in addition to the established effect of spectral similarity.

First, we notice that the phase of the frequency components in each axial signal is not considered by current 321 algorithms. Accordingly, participants could potentially use distortion in the relative phase information when judging similarity; phase changes shift signals in time and therefore might affect temporal matching. Several decades ago, researchers suggested that two
groups of PCs might exist. Even though one PC may not easily distinguish the direction of vibrations [13], the groups could respond to different phases of stimuli [46]–[48] and could thus work together to obtain some phase-related information that is distorted by all of the tested 321 algorithms. Later psychophysical research, however, has reported that the effect of phase-related differences has no significant influence on perception. According to Bensmaia and Hollins, humans cannot perceptually discriminate superimposed sinusoidal vibrations at two frequencies felt via the PC channel (100 and 300 Hz) with different phase shifts [49]. As a result, researchers now generally agree that phase-related information is perceptually unimportant and that perception of such high-frequency vibrations is dominated by magnitude-related information [50]–[52]. We thus believe that phase information could have played a role in our study only for lower frequencies and not for the PC channel.

In this regard, our second hypothesis for the vertical gaps between ORI and the other stimuli in Fig. 8 arises from the different directionality of 1D and 3D vibrations. In our implementation, even 321 algorithms with high spectral matching scores create only single-axis vibrations along the z-axis, while the original recordings output vibrations across all 3D axes. In this regard, Brisben et al. found that the direction in which a grasped physical object vibrates does slightly but consistently affect the absolute threshold for vibration detection [53]. They conducted several psychophysical experiments using a custom cylindrical motor-operated probe with vibration stimuli at either 40 Hz or 300 Hz, finding that participants were slightly more sensitive to vibration movements parallel to the skin than to vibration movements perpendicular to the skin. Thus, we believe that the 3D nature of ORI stimuli might have caused them to feel fundamentally different from all of the 1D stimuli. Indeed, recent work by Serhat and Kuchenbecker used a detailed 3D finite element model of the human fingertip to show that changing the direction of an oscillatory force applied at the center of the fingerpad can greatly affect the resulting tissue deformations both locally and at a distance [54]. PCs or other mechanoreceptors distributed over the large contact area of the precision grip posture (such as Ruffini endings through the SA II channel for sensing skin stretch at 0.5–400 Hz or Meissner’s corpuscles through the FA I channel for fluttering sensations from the shearing force at 3–40 Hz; see [14] for details) may decode relevant directional information from the rendered vibration.

Our third hypothesis is that the dimensionally reduced vibration stimuli may have been perceived as different from the original signals due to technical artifacts in our approach to rendering 1D and/or 3D vibrations, such as rotational motion, vibrational crosstalk between the axes, or audible cues. We tried to limit these artifacts during the study design process, but they cannot be completely eliminated from consideration.

C. Future Work

Importantly, all three of our possible explanations may have contributed to our finding that none of the tested 321 algorithms could produce 1D vibrations that feel the same as the original 3D recordings. In-depth studies with a wider variety of stimuli would be needed to test our hypotheses and determine their relative impacts on the perceptual performance of both existing and new 321 algorithms. For example, we suggest also presenting the original 3D vibration with axes swapped or with other reflections and rotations to determine whether such directional distortions are perceivable even when the spectral match and temporal match metrics are high.

One interesting finding is the relative positions of SUM in the physical-perceptual spaces. In our results, the vertical displacement of SUM from ORI varied depending on the type of interaction and the type of surface, more arbitrarily than other algorithms. We speculate that due to the summation of multiple axes in SUM, the phase-related information of the original signal can be randomly dispersed, e.g., some of the phase data may be canceled or even doubled. Yet, no existing algorithm takes phase-related information into account, and even DFT is biased to focus on the amplitude-related information. Finding a way to preserve the phase information of the original signal as well as matching the frequency spectrum would be a good direction for future research on 321 algorithms. We believe it should be possible to update DFT to improve its performance in this regard.

Except for SAZ and VM, the horizontal differences between DFT and other advanced 321 algorithms (SUM and PCA) were smaller than the vertical difference to ORI, suggesting that humans have a poorer ability to perceptually distinguish differences in the spectral magnitude than the differences induced by present approaches to dimensional reduction. As an alternative explanation to the three hypotheses already presented, the lower temporal match scores we observed may partially stem from the design of the metric itself; we assigned $M_{\text{dim}} = 1$ for ORI, but a 1D signal may not be able to reach this value for some original 3D vibrations. Other ways of quantifying temporal match should thus also be explored. Thinking more broadly, compact and lightweight hardware for generating high-quality 3D vibrations should be investigated as a way of circumventing the need for dimensional reduction in the first place.

VII. Conclusion

This study investigated the perceptual differences between three-to-one dimensional reduction algorithms. We developed a multi-dimensional vibration rendering system using a magnetic levitation haptic interface to output realistic 1D and 3D vibrations. We then collected a dataset of real vibrations from two representative actions (tapping and dragging) with four surfaces having different hardness and roughness. Using the developed system, we rendered the original 3D and the 1D vibrations converted by five different 321 algorithms and obtained their spectral and temporal matching scores. We proceeded to a user study with multiple pairwise comparisons of a subset of the same vibration stimuli. Then, we analyzed the results with MDS to obtain 2D perceptual spaces visualizing the perceptual differences between the original and 321-converted vibrations.
We found strong evidence of a sensory-physical relationship in multi-dimensional vibrations; the perceived dissimilarities are related to the physical dissimilarities based on features of the vibrations. Therefore, algorithms that seek to the spectral difference (like DFT) can still be considered the best 321 approach when perceptual similarity is prioritized, particularly for offline processing. Nevertheless, we also found that even the best available algorithms have a perception gap between the original vibration and the 321-converted vibrations. It remains to be seen whether any 1D vibration can completely imitate the feel of original, realistic 3D vibrations as would be desired for many applications in virtual reality and teleoperation.

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