Normal Left Ventricular Torsion Mechanics in Healthy Children: Age Related Changes of Torsion Parameters Are Closely Related to Changes in Heart Rate

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Background and Objectives: This study was aimed at assessing left ventricular torsion (LVtor) mechanics using speckle tracking echocardiography (STE), establishing normal reference values of principal LVtor parameters, and analyzing the age-related changes in normal children.

Subjects and Methods: Eighty children (aged 3 months to 15 years) with normal cardiac function and rhythm were recruited. LVtor parameters including rotations, twist and untwist, torsion, and their rate indices were measured using STE. Age and heart rate related changes of the parameters were analyzed.

Results: Speckle tracking echocardiography analyses for LVtor parameters had excellent reliability in 64 of 80 subjects (80%) (intraclass correlation coefficients; 0.93–0.97). Early systolic twist (EST) motions (-8.4±0.1°) were observed in all subjects during an early 20±7% of systolic time intervals. The peak systolic twist and torsion were 17.0±6.5° and 2.9±1.3°/cm, respectively. The peak twist velocity was recorded at 51±13% of systolic time and the peak untwist velocity at 13.8±11.5% of diastolic time intervals. Multivariate analysis showed that heart rate change was an independent predictor of changes in torsion parameters; significantly decreasing LV length-normalized apical and basal rotation, torsion, and twist and untwist rate with increasing age. Isovolumetric recoil rate was independent of change in age and heart rate.

Conclusion: Left ventricle showed unique torsion mechanics in children with EST, torsion, and untwists. Heart rate was an independent predictor of the change in torsion parameters with aging. (Korean Circ J 2015;45(2):131-140)

KEY WORDS: Ventricular function; Speckle tracking echocardiography; Torsion; Rotation; Child.

Introduction

Left ventricular (LV) myocardial contraction and relaxation causes a twist and untwist motion due to the helical arrangement of myocardial fibers in the subendocardium and subepicardium of the LV.1-2 As viewed from the apex, the LV apex makes a counterclockwise rotation while the base of the LV makes a clockwise rotation during ventricular systole, and vice versa during ventricular diastole, resulting in LV twist or torsion and untwist motion during the cardiac cycle.2-3 Understanding of the three-dimensional (3D) LV deformation movements has provided a new insight into the ventricular functions that were previously unavailable with conventional analysis of LV contraction of the long and short axis.2-4 Various techniques such as implanted radiopaque markers, biplane cine angiography, sonomicrometry, optical devices, magnetic resonance imaging (MRI), and echocardiography using tissue Doppler imaging have been used to explore LV twist motion in experimental and clinical settings, with limitations to clinical applicability.2-7 Recent improvements in ultrasound technique using two-dimensional speckle tracking echocardiography (2D STE), a novel imaging technique for quantifying complex 3D cardiac motions, has the advantage of angle independency for easier measurement of LV twist.
and untwist movements. This technique was validated with sonomicrometry and tagged MRL.\textsuperscript{8-12} Several reports on LV torsion (LVtor) mechanics using STE and the age-related changes in normal children and adolescents have significant inter-study discrepancies.\textsuperscript{13-16}

Accordingly, we assessed the feasibility of 2D STE in measurement of LVtor mechanics, determined normal reference values of principal parameters of LVtor, and analyzed the age-related changes in normal healthy children.

**Subjects and Methods**

**Study population**

A total of 80 healthy children, aged 3 months to 15 years, were included in the study. They were referred to the cardiac outpatient clinic for echocardiography due to heart murmur, nonspecific chest pain, palpitation, dizziness or syncope, or history of a sibling with congenital heart disease. Comprehensive echocardiography according to our protocol confirmed normal cardiac structure and function, except for patent foramen ovale or trivial degree of tricuspid regurgitation. All subjects had normal sinus rhythm. The body weight and height of all subjects were recorded and the body surface area was derived. The Institutional Review Board of Seoul St. Mary’s Hospital approved this study.

**Echocardiographic assessment**

All echocardiographic assessment and STE image acquisition were done by one designated pediatric cardiologist, using the Vivid 7 ultrasound machine (GE Medical Systems, Horten, Norway). Key images acquired for at least 3 cardiac cycles were saved to customized EchoPAC software (version 7.1; GE Medical Systems, Horten, Norway) for off-line analysis. All echocardiographic indices or images were obtained during a dominant heart rate ±5 beats per minutes in each subject for the optimization of time intervals between images during the cardiac cycle. Each time interval of events (events timing) was normalized by each cardiac cycle length to adjust to heart rate, as previously stated. LV length was defined as the length between LV apical endocardium and the mitral valve annular line. All subjects had normal sinus rhythm. The body weight and height of all subjects were recorded and the body surface area was derived. The Institutional Review Board of Seoul St. Mary’s Hospital approved this study.

**Reproducibility**

Twenty-five subjects were randomly selected to assess intra- and interobserver variability for LVtor measurements. Two independent observers reanalyzed the data sets of apical rotation, basal rotation,
Statistical analysis

Data were analyzed using commercially available software, PASW Statistics (version 18 for windows; IBM, Armonk, NY, USA). Quantitative data were expressed as the mean±standard deviation. The associations between age, heart rate and each echocardiographic parameter were analyzed by Bivariate correlations with Pearson’s correlation coefficients; age and heart rate were entered as covariates to predict changes in each torsion parameter in the multivariate regression analysis. The intra- and interobserver variability was evaluated using the reliability analysis providing intraclass correlation coefficients. A p<0.05 was considered statistically significant.

Results

Feasibility and reproducibility of speckle tracking echocardiography analysis for left ventricular torsion

A total of 80 children with good echocardiographic images for speckle tracking were included in the STE analyses for LVtor parameters.
Among them, good speckle tracking and reliable measurements of torsion parameters were possible in 64 subjects (80%), who finally comprised of the study population for analysis. Demographic and routine standard echocardiography data were summarized in Table 1. The intra- and interobserver variability for LV basal rotation, apical rotation, and peak LV ST were assessed using reliability analysis. The results showing intraclass correlation coefficients >0.9 in all analyses with robust statistical significance were summarized in Table 2.

### Table 1. Demographic and conventional echocardiography data

| Variables | Value, mean±SD |
|-----------|---------------|
| Demographic data | |
| Male:female | 42:22 |
| Age (year) | 6.8±4.2 |
| Body weight (kg) | 27±16 |
| Body surface area (m²) | 0.9±0.4 |
| Heart rate (beats/min) | 91±17 |
| Pulse-wave Doppler | |
| Early diastolic peak velocity (E) (m/s) | 1.09±0.16 |
| Late diastolic peak velocity (A) (m/s) | 0.59±0.14 |
| E/A ratio | 1.94±0.47 |
| MV E deceleration time (ms) | 139±20 |
| LV myocardial performance index | 0.24±0.07 |
| Tissue Doppler imaging (TDI) | |
| MV septal annular systolic velocity (S) (m/s) | 0.07±0.01 |
| MV septal annular early diastolic velocity (E) (m/s) | 0.13±0.02 |
| MV septal annular late diastolic velocity (A) (m/s) | 0.06±0.02 |
| E'/A' ratio | 2.26±0.72 |
| LV myocardial performance index by TDI | 0.42±0.08 |
| E/E' ratio | 8.58±2.18 |

LV: left ventricle, MV: mitral valve

### Table 2. Intraobserver and interobserver variability test (n=25)

| Intraclass correlation coefficients | 95% CI | p |
|------------------------------------|-------|---|
| Basal rotation | 0.96 | 0.92–0.98 | <0.001 |
| Apical rotation | 0.95 | 0.89–0.98 | <0.001 |
| Peak systolic twist | 0.97 | 0.94–0.99 | <0.001 |
| Basal rotation | 0.95 | 0.88–0.98 | <0.001 |
| Apical rotation | 0.93 | 0.85–0.97 | <0.001 |
| Peak systolic twist | 0.96 | 0.92–0.98 | <0.001 |

CI: confidence interval

### Table 3. LV torsion data from speckle tracking echocardiography

| Variables | Value, mean±SD |
|-----------|---------------|
| Early systolic twist | |
| Basal rotation (deg) | 3.4±1.9 (0.1–7.5) |
| Apical rotation (deg) | 13.9±5.0 |
| Peak early systolic twist (deg) | -3.3±1.7 (-8.4–-0.1) |
| Peak early systolic torsion (deg/cm) | -6.0±0.3 (-18.0–-0.3) |
| Time to peak early systolic torsion (% ST) | 20±7 (3–33) |
| Systolic twist | |
| Basal rotation (deg) | -5.0±1.6 |
| Apical rotation (deg) | 13±5.0 |
| Peak systolic twist (deg) | 17.0±6.5 |
| Peak systolic torsion (deg/cm) | 2.9±1.3 |
| Peak systolic twist velocity (deg/s) | 142±48 |
| Peak torsion velocity, (deg/s)/cm | 249±11.0 |
| Time to peak twist (% ST) | 92±5 |
| Time to peak twist velocity (% ST) | 51±13 |
| Diastolic untwist | |
| LV untwisting during IVRT (deg) | -3.4±2.5 |
| LV untwisting velocity during IVRT (deg/s) | -98±66 |
| Isovolumic untwisting recoil (%) | 20±15 |
| Isovolumic untwisting recoil rate (%/ms) | 0.55±0.38 |
| Peak untwisting velocity (deg/s) | -158±0.61.4 |
| Peak untwisting velocity-N, (deg/s)/cm | -27.6±12.8 |
| Time to peak untwisting velocity (% DT) | 13.8±11.5 |

*pLV untwisting during IVRT/peak LV twist<100, †Isovolumic untwisting recoi/IVRT. LV: left ventricular, ST: systolic time, N: normalized by left ventricular length, IVRT: isovolumic relaxation time, DT: diastolic time

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(Figs. 1 and 3, Table 3). The LV EST or EStor were not correlated with increasing age (Fig. 3). The time interval from the onset of LV contraction to the peak LV EST was 19.1±6.9% of the total systolic time (Fig. 1), which did not change with increasing age.

**Left ventricular mid- and late systolic events**

All subjects showed clockwise basal rotation (range; -12.9—1.4°) and counterclockwise apical rotation (range; 3.1—28.7°) during mid- and late systole (Figs. 1 and 4, Table 3). The rotation angle from baseline was significantly greater in the apical segment than in basal segment (13.9±5.0° vs. 5.0±2.6°, p<0.001). Peak apical counterclockwise rotation velocity was faster than peak basal clockwise rotation velocity (101.3±37.6° vs. 82.8±25.9°, p<0.001). When normalized by LV length, both apical and basal rotation decreased with aging (Fig. 4). LV ST began at 20±7% of systolic time (after the EST) and ended at 92±5% of systolic time (Fig. 1, Table 3). The peak ST was not correlated with increasing age, but LVTor decreased with aging (Fig. 5). The peak LV twist velocity was recorded at 51±13%
of systolic time, and decreased with increasing age when normalized by LV length (Fig. 6).

**Left ventricular diastolic events**

Given that LV ST motion ended at $92\pm5\%$ of systolic time, LV untwist motion began before the AVC and reached peak untwisting velocity at $13.8\pm11.5\%$ of diastolic time (Fig. 1, Table 3). Peak untwisting velocity decreased with increasing age when normalized by LV length (Fig. 6). Isovolumic untwisting recoil (LV untwist during IVRT) was $20\pm15\%$, and the isovolumic untwisting recoil rate was $0.55\pm0.38%/ms$, which was unchanged with increasing age.

Correlations and age related changes

The peak LV ST showed good correlations with systolic basal and apical rotation, peak basal and apical rotation velocity, peak ST velocity, and peak untwisting velocity (Table 4). EST, isovolumic untwisting recoil, or recoil rate was not correlated with the peak LV twist.

Table 5 shows correlations of torsion parameters with age and heart rate. Most torsion parameters including rotations, twist, torsion, and velocity parameters showed significant correlation with age and heart rate. However, multivariate analysis showed that the only heart rate was an independent predictor of the torsion parameters (Table 5). Parameters during IVRT including LV untwisting velocity during IVRT, isovolumic untwisting recoil, isovolumic untwisting recoil rate did not show any significant correlations with age and heart rate. Time to peak untwisting velocity showed good correlation with heart rate, but other event timings were constant throughout aging and not correlated with heart rate.

**Discussion**

We assessed LV torsion deformation using 2D STE in healthy infants and children (aged 3 months to 15 years) and described their characteristics in detail. The major findings were as follows: during early systolic periods (about 20% of systolic time) including IVCT, a transient early systolic negative twist or torsion with a direction opposite to the dominant late ST was observed in all subjects; during mid- and late systole, basal clockwise rotation and apical counterclockwise rotation was observed in all subjects, resulting in positive LV twist, which decreased with aging when normalized to LV length; the peak LV twist occurred around 90% of systolic time with peak twist velocity around 50% of systolic time; LV untwist began late systole with 20% untwisting during IVRT, and showed peak untwisting velocity during early diastolic time; and the peak twist and untwisting velocity decreased with aging when normalized by LV length.

**Table 4. Correlations between peak LV systolic twist and other variables**

| Variables                  | Peak LV twist |
|----------------------------|--------------|
| Early systolic twist       | 0.122        |
| Systolic basal rotation    | -0.492       |
| Systolic apical rotation   | 0.860        |
| Peak basal rotation velocity | -0.341      |
| Peak apical rotation velocity | 0.549        |
| Peak systolic twist velocity | 0.805        |
| Peak untwisting velocity   | -0.685       |
| Isovolumic untwisting recoil | 0.178        |
| Isovolumic untwisting recoil rate | 0.125    |

LV: left ventricular, NS: not significant
length. The feasibility and reproducibility were acceptable.

Feasibility and reliability

It was possible to get good quality STE data sets of basal and apical slices for reliable measurements of torsion parameters in 80% of subjects. There are no previous reports on the feasibility of STE for measuring torsion parameters in only children. Previous reports in adults showed relatively low feasibility (35–75%), which might be a challenging issue in STE measures of torsion mechanics in adults.\textsuperscript{17-19} One study including children and young adults aged 3 to 40 years (53 children <16 years) reported that complete data sets could be obtained in only 66% of controls.\textsuperscript{13} Reliable measurements can be obtained from good quality of 2D images with a good echo window, adequate frame rates, and without dropouts of ultrasound data throughout the cardiac cycle. It is more challenging to obtain good quality 2D images in adults than in children, because of large body size and relatively poor echo window. Our data indicated that measurements of torsion parameters using STE is feasible in children. Additionally, intra- and interobserver reliability were excellent with high intraclass correlation coefficients. These findings suggest that STE is a good imaging modality for assessing complex LV deformation in children.

Early systolic events

During the early systolic period (the first ~20% of systolic time), transient clockwise basal rotation in all subjects, and changing apical rotation pattern from counterclockwise to clockwise apical rotation with aging were observed. Hence an ‘early systolic LV twist’ that was opposite in direction to the dominant LV ST during late systole was observed in all subjects. Some reports have addressed early systolic rotation patterns by using different imaging techniques with inter-study discrepancies.\textsuperscript{8,13,17,19} The reason for this discrepancy remains unclear and has been attributed to the difference in temporal resolution between imaging techniques.\textsuperscript{2,8,11} A similar pattern of early systolic rotation and twist (~2°) was confirmed only by STE in an earlier study using MRI and STE in adults.\textsuperscript{8} Another study in adults by van Dalen et al.\textsuperscript{19} also confirmed the early systolic rotation patterns, in which the magnitude of basal rotation decreased with aging. Takahashi et al.\textsuperscript{13} reported early systolic counterclockwise basal rotation (~4.5°) in children, but did not address apical rotation in their study.

The mechanism of the EST motion is explained by a time delay in an electrical activation, thereby leading to a physiological asynchrony of mechanical shortening between the subendocardial and subepicardial regions.\textsuperscript{10,18} Because of the sequential transmural spread

| Table 5. Correlations of torsion parameters with age and heart rate |
|-----------------------------|--------|-----------------------------|--------|-----------------------------|--------|
| Variables                  | Univariate p* | Multivariate p† | Variables                  | Univariate p* | Multivariate p† |
| Torsion parameters         |        |                | Age                     |        |                | Age                     |        |                |
| Peak basal rotation (deg/cm) | 0.003  | <0.001         | NS                     | 0.03   || Peak apical rotation (deg/cm) | 0.006  | <0.001         | NS                     | 0.012   |
| Peak basal rotation velocity (deg/s) | 0.016  | <0.001         | NS                     | <0.001  || Peak apical rotation velocity (deg/s) | 0.005  | NS                     | 0.001   |
| Peak systolic torsion (deg/cm) | 0.003  | <0.001         | NS                     | 0.008   || Peak systolic twist velocity (deg/s) | NS     | NS                     | 0.001   |
| Peak torsion velocity, (deg/s)/cm | <0.001 | <0.001         | NS                     | <0.001  || Peak untwisting velocity (deg/s) | 0.028  | 0.001         | NS                     | <0.05   |
| Peak untwisting velocity-N, (deg/s)/cm | <0.001 | <0.001         | NS                     | <0.001  || LV untwisting velocity during IVRT (deg/s) | NS     | NS                     | NS   |
| Isovolumic untwisting recoil (%) | NS     | NS                     | NS                     | NS   |
| Isovolumic untwisting recoil rate (%/ms) | NS     | NS                     | NS                     | NS   |
| Events timing              |        |                | Age                     |        |                | Age                     |        |                |
| Time to peak early systolic torsion (% ST) | NS     | NS                     | NS                     | NS   |
| Time to peak twist (% ST) | NS     | NS                     | NS                     | NS   |
| Time to peak twist velocity (% ST) | NS     | NS                     | NS                     | NS   |
| Time to peak twist (% ST) | NS     | NS                     | NS                     | NS   |
| Time to peak twist velocity (% ST) | NS     | NS                     | NS                     | NS   |
| Time to peak untwisting velocity (% DT) | NS     | 0.002         | NS                     | 0.001   |

*Bivariate correlation analysis, *Multivariate linear regression analysis. N: normalized by left ventricular length, IVRT: isovolumic relaxation time, ST: systolic time, DT: diastolic time, LV: left ventricular.
of electrical activation from the subendocardial to subepicardial region, the shortening of inner subendocardial fibers with right-handed helix is accompanied by stretching of the outer subepicardial fibers with left-handed helix during IVCT.\(^{12,20,21}\)

We firstly confirmed that the LV during childhood, although not fully matured, also showed a unique pattern of rotation and twist during the early systolic period.

**Left ventricular mid- and late systolic events**

We also demonstrated a uniform LV counter clockwise apical and clockwise basal rotation, and a 'positive' LV twist or torsion during mid- and late systole as previously reported. However, the magnitude of rotations, twist, and torsion, and age related changing patterns of these parameters were quite different from previous studies.\(^{7,13-15}\) Takahashi et al.\(^{13}\) reported normal values of torsion parameters in 111 volunteers including 53 children (3–16 years), and showed mean peak LV twist of around 11°, and mean peak LVtor around 1.65°/cm, which were lower in magnitude compared to our study (peak ST; 17.0±6.5°, peak systolic torsion; 2.9±1.3°/cm). The magnitude of basal rotation was similar, but apical rotation of their study was smaller, with a smaller peak LV twist, as compared to our study. Zhang et al.\(^{13}\) also reported normal data in children with much smaller magnitudes of rotation and twist values than our results. The reason for these discrepancies between studies is not clear and may be a major limitation to STE for LVtor movement measures. Furthermore, these reported data may not be useful as reference values in clinical practice.

Because the rotation angle in a cylinder is proportional to shaft length, the farther the slice from the equator level, the greater rotation angle recorded even in the same heart.\(^{25}\) Additionally, since the equator level of LV twist is around one-third of LV length from the LV base, the magnitude of LV apical rotation is greater than that of basal rotation.\(^{25}\) One possible explanation for the inter-study discrepancies is difference in image acquisition sites for STE analysis, especially the position of LV apical slice sampling. Parisi et al.\(^{14}\) compared LVtor measurements between 2D and 3D STE in 30 healthy subjects, and demonstrated that the 2D LV apical level acquisition, even when recorded in a standard manner, determines variability of measurements; the twist value was higher when the apical rotation was measured from an apical section closer to the apex. We made every effort to get adequate images in terms of sampling position of as close as possible to the LV base and apex for each image slice, which may explain the higher values of LV twist motions. Thus, current anatomical markers for image acquisition adopted from the previous studies need to be redefined to overcome the pitfalls of this imaging technique.

**Diastolic events**

Diastolic untwist begins immediately after the peak ST, actually before closure of the aortic valve, and reaches its peak velocity during early diastolic period. A significant amount of untwisting occurs in the early diastolic period, especially IVRT (about 20% in this study). These findings were consistent with the previously reported results.\(^{13-15,20}\) Myocardial relaxation is dependent on the rates of cross-bridge deactivation within the sarcomere and is associated with the release of restoring forces stored in the ventricular wall during diastole.\(^{20}\) Rapid LV untwisting during early diastole decrease in LV pressure rapidly during IVRT and enables the LV to suck blood effectively during mitral valve opening. Dong et al.\(^{20}\) reported that the isovolumic untwisting recoil rate was closely correlated (r = -0.86, p<0.0001) with the relaxation time constant (τ), independent of loading conditions, in an animal study using MRI tagging. They suggested that this noninvasive parameter could be a good tool for preload independent assessment of LV relaxation.\(^{20}\) We also derived the isovolumic untwisting recoil rate (0.55±0.38%/ms) using STE, which was constant throughout aging, and might be a handy tool to assess LV diastolic function in various clinical settings.

**Correlations and age related change**

The peak LV basal and apical rotation, and twist did not change with increasing age, but decreased significantly with aging when normalized by LV length. The LV peak twist and untwisting velocity normalized by LV length decreased significantly with aging. Previous reports on the changing patterns during childhood also showed significant inter-study discrepancies of unexplained reasons.\(^{7,13-15}\) We speculated that differences in the position of imaging acquisition for each apical and basal slice may partially explain inter-study discrepancies.

The mechanism of age related changes in torsion mechanics have been attributed to changing or maturation patterns of calcium transport into the sarcoplasmic reticulum, alterations in connective tissue and relative proportions of 2 titin isoforms (N2B and N2BA), which are responsible for elastic recoil within the sarcomere, and change in relative contributions of subendocardial and subepicardial myocardium to age-related LVtor mechanics.\(^{7,13,15}\) However, while reasonable to speculate, it is difficult to directly prove the associations between the physiologic or histopathologic changes in LV and aged-related LVtor mechanics. We clearly and firstly demonstrated by multivariate analysis that the change in heart rate is responsible for changes in LVtor mechanics, especially velocity profiles during childhood.

Event timings may increase with aging along with decrease in heart rates.\(^{13,14,19}\) However, all event timings including time to peak twist, torsion, peak ST velocity, and peak diastolic untwisting velocity were

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constant with childhood ages when standardized with cardiac cycle length (systolic and diastolic time intervals). Given that heart rate change is significant during childhood, especially during infancy, it should be incorporated into the analyses of LV mechanics. Interestingly, isovolumic untwisting recoil and isovolumic untwisting recoil rate were independent of changes in age and heart rate. This finding was consistent with the result by Dong et al.,\(^{29}\) and may provide a novel parameter of assessing LV relaxation.

Clinical implications

Clinical application of torsion parameters is still limited but emerging. Cheung et al.\(^{26}\) studied LV\(_{\text{tor}}\) mechanics in 36 childhood cancer survivors, and found that impairment of LV\(_{\text{tor}}\) mechanics is evident in children after anthracycline therapy, even in those with “normal” LV EFs. Another recent study on 14 children with genotype-positive, phenotype-negative hypertrophic cardiomyopathy (HCM) showed that children with genetically proven HCM had increased LV rotation and twist, as compared to normal controls, before the development of hypertrophy.\(^{27}\) The authors suggested that apical rotation by STE may be a clinically useful early marker of HCM before the onset of hypertrophy.\(^{28}\) Additionally, Khoo et al.\(^{29}\) reported that patients with normal LV EFs and cardiovascular magnetic resonance features of myocarditis had altered LV\(_{\text{tor}}\) parameters when compared to normal controls. These results collectively suggest that the novel echocardiographic torsion parameters may improve early detection of patients with important “subclinical” LV dysfunction in various clinical settings.\(^{29}\)

Limitations

Since this study was done in children up to 15 years of age, some subjects needed medications for sedation such as chloral hydrate, which might have influenced the LV function, heart rate, or blood pressure, thereby leading to change in LV\(_{\text{tor}}\) mechanics. The other important limitation of this study was associated with the fundamental drawback of 2D STE, in which the levels of image acquisition for the basal and apical rotation could not yet be clearly defined. However, all efforts were made to get good quality images, and to get imaging slices as far as possible from the equator level of LV twist that may provide more accurate parameters of LV\(_{\text{tor}}\) mechanics. Thus, current anatomical markers for image acquisition as described in the previous studies may be redefined to overcome the pitfalls of this imaging technique.

Conclusions

We assessed and described LV\(_{\text{tor}}\) mechanics in detail with the determination of normal reference values of LV\(_{\text{tor}}\) parameters in children aged 3 months to 15 years. Although not fully matured, LV in infants and children also showed unique torsion mechanics, including early systolic negative twist during IVRT, systolic positive twist, and early diastolic untwist. Age related changes of rotation, torsion, and velocity parameters were evident and closely related to changes in heart rate with increasing age.

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