Al-Based porous coordination polymer derived nanoporous carbon for immobilization of glucose oxidase and its application in glucose/O2 biofuel cell and biosensor†

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Herein, we report the first example of using the Al-based porous coordination polymers (Al-PCP) as a template for preparation of nanoporous carbon through a two-step carbonized method. By applying the appropriate carbonized temperature in the first-step carbonization process, both high surface area and large pore volume are realized in the second-step carbonization process even at a high-temperature. The SEM images show that the carbonized Al-PCP before and after HF treatment (PCP) retained mostly crystallite shapes and sponge-like surface morphology. The TEM images of carbonized Al-PCP and PCP clearly exhibited high porosity with a wide range of pore sizes spanning from micro- to macropores. The maximum BET surface area and pore volume were 2773.5 m² g⁻¹ and 1.885 cm³ g⁻¹, respectively. The obtained highly nanoporous carbon PCPs were used to modify a glassy carbon electrode (GCE) based on glucose oxidase (GOx), resulting in efficient direct electron transfer and excellent bio-catalytic performance. In addition, a glucose/O2 fuel cell constructed using Naﬁon/GOx/PCP/GCE as the anode and an E-TEK Pt/C modiﬁed GCE as the cathode generated a maximum power density of 0.548 mW cm⁻² at 0.41 V. The findings in this work may be helpful for exploiting novel nanoporous carbons derived from metal–organic framework (MOF) by using a two-step carbonization method for the immobilization of enzymes in enzymatic biofuel cells or biosensors.

1. Introduction

Enzymatic biofuel cells (EBFCs) are considered promising, environmentally friendly and green energy devices, which are capable of harvesting electrical energy from renewable and abundantly available biofuels by using redox enzymes as the catalysts for oxidation of biofuels and reduction of oxidizers.1–4 However, efﬁcient electron transfer between the active sites of enzymes and the current collector or the electrode is not efﬁcient, mostly because the active sites of enzymes are embedded in the electrical insulation of protein shells.5,6 Therefore, it is necessary and desirable to establish an effective bioelectrocatalytic system for oxidation of biofuels for biofuel cells.8 Glucose oxidase (GOx) is one of the most commonly considered enzymes for bioanode in biofuel cells, because it can oxidize glucose directly to gluconolactone in a two-electron transfer step.7–10 Judicious choice of the biocompatible materials for immobilization of GOx is the key step to construct a bioanode.11,12 Therefore, exploring new electrode materials for the immobilization of GOx is highly desirable for biofuel cell construction.

Over the past few years, nanomaterials with high electrical conductivity, large speciﬁc surface area and high porosity have been introduced as supporting materials for immobilizing the GOx molecules.13–16 Among the various nanomaterials, carbon nanotubes (CNTs) and graphene (Gr) have been attracted enormous attentions for immobilization of GOx owing to their excellent physicochemical properties.4,14,16,17 Hence, extensive efforts have been put forward to achieve synergistic integration of three-dimensional (3D) CNTs network or Gr with other nanomaterials as supporting materials for enzyme immobilization.4,14,18–20 While these nanomaterials produce successful electrode architectures with a more reliable attachment scheme and greater enzyme density using more convenient materials.

Recently, metal–organic frameworks (MOFs) or porous coordination polymers (PCPs), as typical inorganic–organic hybrids, have been used as templates/precursors to prepare porous carbons through thermal conversion.21–23 MOFs-templated carbons have attracted great attention because of
their exceptionally high surface areas and the ability to control their pore textures.\textsuperscript{24} The MOFs-derived nanoporous carbons (NPCs) are promising for a variety of applications, such as contamination removal,\textsuperscript{25} gas/liquid storage,\textsuperscript{22,24} supercapacitors\textsuperscript{23,26} and fuel cell systems. In the EBFCs fields, the NPCs materials for immobilization of enzymes are mostly prepared by template methods using mesoporous silica or zeolites as templates.\textsuperscript{27–29} Compared with the traditional porous materials, MOFs are unique in terms of their extraordinarily high porosity, tunable pores, and diverse functional sites.\textsuperscript{30,31} However, the MOFs-derived NPCs have barely been reported for the application in EBFCs.

In this paper, we selected a typical Al-based porous coordination polymer (Al-PCP) as a precursor to synthesize the NPCs by a two-step carbonized method. The Al-PCP powders were first carbonized at 800 °C, and the obtained product Al-PCP\textsubscript{800} (800 is the carbonized temperature) was washed extensively with an HF solution to remove the residual Al component. Then the PCP\textsubscript{800} was calcined again at various temperatures from 1000 to 1600 °C under an inert gas. The obtained samples were denoted as “PCP\textsubscript{x}”, where the x is applied calcination temperature of the second-step carbonized process. Then the electrochemical performance of the PCP\textsubscript{x} as a novel substrate for immobilization of GOx were studied.

2. Materials and methods

2.1. Materials

Glucose oxidase (GOx, EC 1.1.3.4, from \textit{Aspergillus niger}, 200 U mg\textsuperscript{-1}) and Nafion solution (5 wt%) were purchased from Sigma-Aldrich and used as received. 1,4-NDC were purchased from Alfa-Aesar and pretreated as received. E-TEK Pt/C (20 wt%) catalyst was purchased from De Nora Elettrodi. Glucose, ascorbic acid (AA), uric acid (UA) and other conventional reagents were obtained from Sinopharm Chemical Reagent Co., Ltd. (China). All reagents were of analytical grade and used without further purification. Phosphate buffer solutions (PBS, 0.1 M, pH = 7.2) were prepared with 0.1 M NaH\textsubscript{2}PO\textsubscript{4} and 0.1 M Na\textsubscript{2}HPO\textsubscript{4}. Different stock solution concentrations of glucose were prepared by 0.1 M PBS (pH 7.2) and mutarotated at least 24 h before use. All solutions were prepared with deionized water which was purified with a Millipore-Q purification system to a specific resistance over 18.0 MQ cm.

2.2. Synthesis of nanoporous carbon

Al-PCP powders were prepared according to the previous report.\textsuperscript{31} Two-step carbonization method was carried out by means of gradual heating (heating rate is 2 °C min\textsuperscript{-1}) up to the target temperature in argon atmosphere and maintained for 4 h. The applied carbonization temperature in first-step was 800 °C and
referenced to the works of Hu et al. After calcination, the obtained black powder Al-PCP800 was immersed in 20% HF under magnetic stirring for 48 h to remove the residual Al component. Then the turbid liquid was centrifuged and the precipitate was washed extensively with deionized water, then the black powder PCP800 was dried under vacuum condition for 8 h at 60 °C. After that, the obtained black powder PCP800 was calcined again with applied calcination temperatures varying at 1000, 1200, 1400 and 1600 °C, respectively.

2.3. Fabrication of GOx modified electrode based on PCPx

For preparing a GOx electrode, a glassy carbon electrode (GCE) was sequentially polished by using slurry of 0.5 μm and 0.03 μm alumina power and successively washed by ultrasonication in deionized water, 1 M HNO₃, deionized water and ethanol for 3 minutes, respectively. Then the electrode was activated electrochemically in 0.1 M sulfuric acid by cyclic voltammetry (CV) until the CV curve to invariant. Thereafter, the electrode was abundantly washed with deionized water and dried under argon flow, then 5 μL of the PCP₧ suspension (5 mg mL⁻¹, prepared by deionized water) was dropped on the GCE surface by using a microinjector, and then the electrode was dried in air. The obtained electrode was denoted as PCP₧/GCE. After that, 2 μL of GOx solution (20 mg mL⁻¹, prepared by PBS, pH 4) was spread onto the surface of PCP₧/GCE electrode and then put them in a refrigerator (4 °C) for 6 h. The obtained electrode was denoted as GOx/PCP₧/GCE. Finally, 5 μL of Nafion solution (1 v/v%,
prepared by ethyl alcohol, 99.99%) was spread on surface of GOx/PCP_/GCE. Then put them in a refrigerator (4 °C) for 2 h. The final electrode was denoted as Na+/GOx/PCP_/GCE. For comparison, Na+/GC, Na+/GOx/GC, and Na+/PCP_/GC electrodes were prepared. All prepared enzyme electrodes were stored in PBS at 4 °C when not in use.

2.4. Apparatus and measurements

All electrochemical experiments were carried out by a CHI 660C electrochemical workstation (CHI Instrument, Shanghai, China) using a conventional three-electrode consisting of a modified glassy carbon as working electrode (3 mm in diameter), a Pt sheet with surface area of 1 cm² as counter electrode and an Ag/AgCl (3 M KCl) electrode as reference electrode. The electrochemical measurements were carried out in 0.1 M sodium phosphate buffer solution (PBS, pH 7.2) as the supporting electrolyte, which were purged with high-purity argon for at least 30 min prior to experiments and a argon environment was then kept over the solution in the cell. All experiments were performed at ambient temperature. Spectrum 100 FT-IR from Perkin Elmer was used for the Fourier Transform Infrared Spectroscopy (FT-IR) studies. XRD studies were performed on a PANalytical X’pert Pro X-ray diffractometer. Raman was measured by a WITec CRM200 using 532 nm laser. Scanning electron microscopy (SEM) analysis was carried out using a JSM-6701 field emission scanning electron microscopy (JEOL, Japan) at an accelerating voltage of 10 kV with a Phoenix energy dispersive X-ray analyzer (NS7, Thermo, USA). Transmission electron microscopy (TEM) images were recorded on a JEOL JEM-2100 microscope operated at an acceleration voltage of 200 kV.

2.5. Electrochemical performance of the BFC

Power density measurements were referenced to previous report.¹⁹ To assemble a glucose/O₂ BFC, the PCP-x nanoporous materials modified GC electrode immersed in 0.1 M PBS (pH = 7.2) containing 0.1 M glucose was used as the bioanode and an E-TEK Pt/C modified GC electrode immersed in 0.2 M Britton–Robinson (B–R) buffer (pH = 5) with continuously bumping oxygen was used as the cathode. The E-TEK Pt/C electrode was prepared by casting 10 μL of 10 mg mL⁻¹ commercial E-TEK Pt/C (20 wt%) on the well-polished GC electrode. Naion 117 film was used as a separator (membrane) between two electrodes. Linear sweep voltammetry (LSV) was used to evaluate the performance of BFC.

3. Results and discussion

3.1. Morphology and structure

Fig. 1 shows the SEM images of carbonized Al-PCP₈₀₀ and PCPₓ. As shown in Fig. 1(A), Al-PCP₈₀₀ clearly exhibited mostly crystallite shapes and sponge-like surface morphology with
voids were formed by the gas evolution (mostly CO2, CO, C6H6) fully removed by HF treatment. The more and larger cracks/voids, indicating that Al component was successfully removed by HF treatment. The more and larger cracks/voids were formed by the gas evolution (mostly CO2, CO, C6H6) fully removed by HF treatment. The more and larger cracks/voids, indicating that Al component was successfully removed by HF treatment.

Fig. 2(A) the Al-PCP800 exhibited homogeneous rod-like shape accompanied numerous flocculent structures at margin. The enlargement images further displayed high porosity with a wide range of pore sizes spanning from micro- to macropores. The corresponding high resolution images showed in Fig. S2(A) exhibited highly defective, randomly oriented graphitic type porous carbon. After HF treatment, PCP800 (Fig. 2(B)) retained macroscopic morphology of Al-PCP800 but with more cracks. After the second calcination, PCP (Fig. 2(C), (D) and S1†) all retained the macroscopic morphology of PCP800 suggesting that the macroscopic structure of PCP800 was not destroyed by the second calcination process even at a higher temperature. On the microsporous structure, the PCP tended to graphitize with the increase in calcination temperature. As shown in Fig. S2(C–F),† graphitic layers were becoming more and more obvious, especially in Fig. S2(F).†

For the specific surface areas and pore-size distribution of the samples (Al-PCP800, PCP800, PCP1200, PCP1600) were characterized by using N2 adsorption–desorption isotherms and shown in Fig. 3(A) and (B). As shown in Fig. 3(A), the steep increase in the adsorbed volume of Al-PCP800 at low relative (P/P0 < 0.1) revealed the presence of micropore, and the following small slope at medium relative pressure (0.1 < P/P0 < 0.8) as well as the desorption hysteresis denoted the existence of developed mesopores, while the final almost vertical tail at the relative pressure near 1.0 pointed to the presence of macropore. After the second calcination, PCP (Fig. 2(C), (D) and S1†) all retained the macroscopic morphology of PCP800 suggesting that the macroscopic structure of PCP800 was not destroyed by the second calcination process even at a higher temperature. On the microsporous structure, the PCP tended to graphitize with the increase in calcination temperature. As shown in Fig. S2(C–F),† graphitic layers were becoming more and more obvious, especially in Fig. S2(F).†

The two-step carbonized method can successfully avoid the occurrence of that phenomenon. Fig. 3(C) shows the Raman spectrum of PCP800. The peak at 1350 cm−1 (D-band) is attributed to the vibration of sp2 hybridize carbon atoms, while the peak at 1580 cm−1 (G-band) is attributed to the vibration of sp3 hybridized carbon atoms. The intensity ratio of D-band to G-band (I/D/I) can be used to evaluate the degree of crystallization. The intensity ratios of D-band to G-band (I/D/I) were 1.768, 1.293, 1.166, 1.103 and 0.998 of PCP, (x is from low to high), respectively, suggesting that the degree of crystallization was increased with the increase in calcination temperature and PCP were amorphous carbon. The chemical structure and composition of Al-PCP800, PCP800 and PCP1600 were further studied by XRD and shown in Fig. 3(C). The strong peak at 16.0° in the XRD pattern of the Al-PCP800 was attributed to Al2O3 which was formed by a dehydration reaction of Al(OH)3 parts of Al-PCP under a high temperature. While there was no peak at 16.0° in the XRD pattern of PCP800, indicating that the Al component was sufficiently removed by HF. Several broad peaks were observed at 26.0° and 44° in all patterns, which were belong to a typical (002) interlayer peak of graphitic carbon.

Fig. 4  (A) CVs of (a) PCP800, (b) PCP1000, (c) PCP1200, (d) PCP1400 and (e) PCP1600 modified GCE based on GOx. (B) CVs of (a) Naﬁon/GCE, (b) Naﬁon/GOx/GCE, (c) Naﬁon/PCP1600/GCE. (d) Naﬁon/GOx/PCP1600/ GCE. All experiment were conducted in 0.1 M pH 7.2 PBS, scan rate: 50 mV s−1.

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3.2. Direct electrochemical properties

The direct electrochemical performances of GOx based on PCP modified glassy carbon electrode were investigated by cyclic voltammetry (CV) and shown in Fig. 4(A). Obviously, there were no peaks on the Na\textsubscript{fi}on/GOx/PCP\textsubscript{800}/GCE (curve a) and Na\textsubscript{fi}on/GOx/PCP\textsubscript{1000}/GCE (curve b), while a pair of well-defined redox peaks were observed at the others electrodes (curve c–e) and the higher carbonized temperature the larger peak current. Especially, the redox peak separation (\(\Delta E\text{p}\)) of Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE (curve e) was estimated, indicating a high-efficient electron transfer rate. Hence, the Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE was used as the model electrode in the subsequent experiments.

Fig. 4(B) shows the CVs of Na\textsubscript{fi}on/GCE (curve a), Na\textsubscript{fi}on/GOx/GCE (curve b), Na\textsubscript{fi}on/PCP\textsubscript{1600}/GCE (curve c), Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE (curve e). As expect, no redox peak was observed at the curve a, b and c while a pair of well-defined redox peaks were observed at the curve e, indicating that the redox peak was attributed to the GOx. The reaction mechanism of GOx on an electrode without the interference of oxygen was previously proposed, and the equation was shown below:

\[
\text{GOx}(\text{FAD}) + 2H^+ + 2e^- \rightarrow \text{GOx}(\text{FADH}_2)
\]  

Curve d in Fig. 4(B) displayed a pair of redox peaks with anodic peak potential at \(-0.418\) V and reduction peak potential at \(-0.461\) V. Its formal potential \(E^0\), the average of anodic and reduction peak potentials, was estimated to be \(-0.440\) V, which was very close to that of GOx and its cofactor FAD reported previously, suggesting that the GOx molecules retained their bioactivity after they were immobilized on PCP\textsubscript{1600}. Therefore, all these results indicated that the MOFs-derived nanoporous carbons have tremendous potential for the application in immobilization of enzymes.

The effect of supporting electrolyte pH value on the direct electron transfer of GOx was studied. Fig. 5(A) shows the CVs of Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE in 0.1 M Ar-saturated PBS with various pH values from 5 to 9 at a scan rate of 50 mV s\textsuperscript{-1}. The formal potential \(E^0\) displayed a linear relation to pH with a slope of 57.8 mV per pH (\(R^2 = 0.9986\)) (Fig. 5(B)). This value was very close to the theoretical value of \(-59.2\) mV pH\textsuperscript{-1}, indicating that two-proton and two-electron participated in the transportation process of FAD/FADH\textsubscript{2} redox couples in the GOx. The effect of scan rate on the electrochemical performance of Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE was shown in Fig. 5(C). The redox peak currents increased linearly with the potential scan rate increasing from 50 to 500 mV s\textsuperscript{-1} (Fig. 5(D)), indicating a quasi-reversible surface-controlled electrochemical process. Furthermore, the dependence of anodic and reduction peak potentials on the Napierian logarithm of scan rates was examined and used to determine anodic electrochemical parameters according to eqn (2) and (3):

\[
E_{\text{Pc}} = E^0 - \frac{RT}{aF} \ln \left( \frac{\alpha F n}{RT k_n} \right)
\]  

\[
E_{\text{Pc}} = E^0 + \frac{RT}{(1 - \alpha)nF} \ln \left( \frac{(1 - \alpha) F n}{RT k_n} \right)
\]  

Fig. 5 The pH dependence of CVs (A) and formal potential (B) at Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE electrode at a scan rate of 50 mV s\textsuperscript{-1}; scan rate dependence of CVs (C) and peak currents (D) of Na\textsubscript{fi}on/GOx/PCP\textsubscript{1600}/GCE electrode in 0.1 M pH 7.2 PBS.
where \( E^{\circ} \) is formal potential, \( \alpha \) is charge transfer coefficient of system, \( \nu \) is scan rate, \( n \) is number of electron transfer, \( k_\text{a} \) is heterogeneous electron transfer rate constant, \( T \), \( R \), and \( F \) are as usual meaning. As can be seen from Fig. S3, the peak potential was linear with the Napierian logarithm of scan rates (at a high scan rate), which was consistent to previous reports. Based on these equations, \( n \) and \( \alpha \) were calculated from the slopes. Thus \( \alpha \) and \( n \) are found to be 0.43 and 1.89, respectively. Additionally, \( k_\text{a} \) of the GOx/PCP1600 based system was calculated by eqn (4):

\[
\log k_\text{a} = \alpha \log(1 - \alpha) + (1 - \alpha) \log \alpha - \log \left( \frac{RT}{nF\nu} \right) - \alpha(1 - \alpha) \left( \frac{nFE_\alpha}{2.3RT} \right)
\]

(4)

From the eqn (4), \( k_\text{a} \) was estimated to be 9.5 at 100 mV s\(^{-1}\), which is larger than that in previous reports. According to the Laviron eqn (5):

\[
i_p = \frac{n^2F^2 I^* A}{4RT} \nu
\]

(5)

where \( Q \) is charge integrated from the reduction peak, \( \nu \) is scan rate, \( n \) is number of electron transfer, \( F \), \( R \), and \( T \) are as usual meaning. According to above results, the \( n \) was calculated to be 1.89, which is very close to the theoretical value of 2. Based on Faraday’s law, \( Q = nFE_\alpha \), where \( A \) is effective surface area of the working electrode, \( I^* \) is surface coverage of GOx. \( I^* \) was calculated to be 9.64 \( \times \) \( 10^{-8} \) mol. This loading was almost 2 orders of magnitude higher than similar nanometer materials as previously reported. The higher GOx loading was explained by the high specific surface area and cumulative pore volume of PCP1600.

3.3. Bio-catalytic property of the Nafion/GOx/PCP1600/GCE electrode and its application in biofuel cell

Fig. 6(A) shows the CV curves of Nafion/GOx/PCP1600/GCE in air-saturated 0.1 M PBS containing different concentrations of glucose at a scan rate of 50 mV s\(^{-1}\). The reduction peak current decreased gradually with increasing glucose concentration. It’s well known that the DET process of GOx is a two-electron and two-proton coupled reaction. The reduction peak current \( I_{p\text{R}} \) is attributed to reduction of GOx(FAD), while the anodic peak current \( I_{p\text{A}} \) is attributed to oxidation of GOx(FADH\(_2\)). Upon addition of glucose, the reduction peak current decreased linearly, which could be attributed to the enzyme-catalyzed glucose oxidation (reaction (6)). The calibration curve (inset in Fig. 6(A)) corresponding to CV response was linear against the glucose concentration ranging from 0.07 to 0.99 mM with a sensitivity of 6.81 \( \mu \)A mM\(^{-1}\). The detection limit was estimated to be about 0.065 mM based on the criterion of a signal-to-noise ratio of 3.

\[
\text{GOx(FAD)} + \text{glucose} \rightarrow \text{GOx(FADH}_2\!) + \text{gluconolactone} \quad (6)
\]

Anti-interference ability of the fabricated electrode of Nafion/GOx/PCP1600/GCE was investigated by introducing electro active species such as AA and UA. Fig. S4† shows \( i-t \) curve of the influence of AA (0.5 mM) and UA (0.5 mM) on the detection of glucose at the applied potential of \(-0.4 \text{ V versus Ag/AgCl} \). When these species were consecutively added into continuously stirred 0.1 M PBS the current response was changed weakly, indicating that Nafion/GOx/PCP1600/GCE exhibited good selectivity for glucose.

The performance of the assembled glucose/O\(_2\) BFC was further investigated under the optimum conditions. Fig. 6(B) shows the current and the power density of the BFC as a function of the operating cell voltage (\( I-V \) and \( I-P \) curves) at a room temperature (25 °C). The open-circuit voltage (\( V_{\text{OC}} \)) and the short-circuit current of the BFC are 0.68 V and 4.46 mA cm\(^{-2}\), respectively. A maximum power density of 0.548 mW cm\(^{-2}\) was obtained at 0.41 V.

4. Conclusions

In this study, we successfully prepared NPCs with a high surface area and large pore volume by a two-step carbonized method of Al-PCP. The obtained PCP\(_{1600}\) exhibited highly hierarchical porous carbons with a high BET surface area up to 2773.5 m\(^2\).
and high cumulative pore volume up to 1.885 cm$^3$ g$^{-1}$. Base on PCP$_{1600}$, a high performance bioanode has been developed successfully. The fabricated electrode of Nafion/GOx/PCP$_{1600}$/GCE showed sufficient DET and good catalytic activity towards glucose oxidation. In addition, a glucose/O$_2$ BFC fabricated by the GOx electrode as the bioanode and a commercial E-TEK Pt/C modified GC electrode as the cathode, delivered a maximum power density of 0.548 mW cm$^{-2}$ at 0.41 V. The two-step carbonized method provides a new example of thermal decomposition of MOFs, which can avoid the collapse of MOF structure at high temperatures. This finding may show tremendous potential for exploring more NPCs derived from MOF family.

**Conflict of interest**

The authors declare no competing financial interest.

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**References**

1. Y. Chen, P. Gai, J. Zhang and J.-J. Zhu, *J. Mater. Chem. A*, 2015, 3, 11511–11516.
2. K. P. Prasad, Y. Chen and P. Chen, *ACS Appl. Mater. Interfaces*, 2014, 6, 3387–3393.
3. M. Rasmussen, S. Abdellaoui and S. D. Minteer, *Biosens. Bioelectron.*, 2016, 76, 91–102.
4. Y. Zhang, M. Chu, L. Yang, Y. Tan, W. Deng, M. Ma, X. Su and X. Xie, *ACS Appl. Mater. Interfaces*, 2014, 6, 12808–12814.
5. M. Ammam and J. Fransaer, *J. Power Sources*, 2014, 257, 272–279.
6. D. Sarauli, K. Peters, C. Xu, B. Schulz, D. Fattakhova-Rohlfind and F. Lisdat, *ACS Appl. Mater. Interfaces*, 2014, 6, 17887–17893.
7. R. Zhao, X. Liu, J. Zhang, J. Zhu and D. K. Wong, *Electrochim. Acta*, 2015, 163, 64–70.
8. L. Qian and L. Lu, *RSC Adv.*, 2014, 4, 38273.
9. Y. F. Gao, T. Yang, X. L. Yang, Y. S. Zhang, B. L. Xiao, J. Hong, N. Sheibani, H. Ghourchian, T. Hong and A. A. Moosavi-Movahedi, *Biosens. Bioelectron.*, 2014, 60, 30–34.
10. Q. Liu, X. Lu, J. Li, X. Yao and J. Li, *Biosens. Bioelectron.*, 2007, 22, 3203–3209.
11. H. U. Lee, H. Young Yoo, T. Limhavgusuren, Y. Seok Song, C. Park, J. Kim and S. Wook Kim, *Biosens. Bioelectron.*, 2013, 42, 342–348.
12. A. A. Babadi, S. Bagheri and S. B. Hamid, *Biosens. Bioelectron.*, 2016, 79, 850–860.
13. J. Chen, R. Zhu, J. Huang, M. Zhang, H. Liu, M. Sun, L. Wang and Y. Song, *Analyst*, 2015, 140, 5578–5584.
14. N. Wang, M. Wen and Q. Wu, *Colloids Surf., B*, 2013, 111, 726–731.
15. J. Liu, C. Guo, C. M. Li, Y. Li, Q. Chi, X. Huang, L. Liao and T. Yu, *Electrochem. Commun.*, 2009, 11, 202–205.
16. R. Zhao, X. Liu, J. Zhang, J. Zhu and D. K. Y. Wong, *Electrochim. Acta*, 2015, 163, 64–70.
17. C. Hou, D. Yang, B. Liang and A. Liu, *Anal. Chem.*, 2014, 86, 6057–6063.
18. J. Balamurugan, T. D. Thanh, N. H. Kim and J. H. Lee, *Biosens. Bioelectron.*, 2016, 83, 68–76.
19. J. Liu, X. Zhang, H. Pang, B. Liu, Q. Zou and J. Chen, *Biosens. Bioelectron.*, 2012, 31, 170–175.
20. S. El Ichi, A. Zebda, A. Laaroussi, N. Reverdy-Bruas, D. Chaussy, M. Naceur Belgacem, P. Cinquin and D. K. Martin, *Chem. Commun.*, 2014, 50, 14535–14538.
21. A. J. Amali, J. K. Sun and Q. Xu, *Chem. Commun.*, 2014, 50, 1519–1522.
22. Y. Li, Y. X. Zhou, X. Ma and H. L. Jiang, *Chem. Commun.*, 2016, 52, 4199–4202.
23. M. Hu, J. Reboul, S. Furukawa, N. L. Torad, Q. Ji, P. Srinivasu, K. Ariga, S. Kitagawa and Y. Yamauchi, *J. Am. Chem. Soc.*, 2012, 134, 2864–2867.
24. A. Aljaz, N. Fujiwara and Q. Xu, *J. Am. Chem. Soc.*, 2014, 136, 6790–6793.
25. L. Wang, F. Ke and J. Zhu, *Dalton Trans.*, 2016, 45, 4541–4547.
26. B. Liu, H. Shioyama, T. Akiha and Q. Xu, *J. Am. Chem. Soc.*, 2008, 130, 5390–5391.
27. E. Magnier, *Chem. Soc. Rev.*, 2013, 42, 6213–6222.
28. Z. Zhou and M. Hartmann, *Chem. Soc. Rev.*, 2013, 42, 3994–3912.
29. Z. Zhou and M. Hartmann, *Top. Catal.*, 2012, 55, 1081–1100.
30. Y. Cui, B. Li, H. He, W. Zhou, B. Chen and G. Qian, *Acc. Chem. Res.*, 2016, 49, 483–493.
31. A. Comotti, S. Bracco, P. Sozzani, S. Horike, R. Matsuda, J. Chen, M. Takata, Y. Kubota and S. Kitagawa, *J. Am. Chem. Soc.*, 2008, 130, 13664–13672.
32. Inamuddin, K. Ahmad and M. Naushad, *Int. J. Hydrogen Energy*, 2014, 39, 7417–7421.
33. G. Srinivas, *Energy Environ. Sci.*, 2013, 7, 335–342.
34. M. Tavviri, H.-A. Rafiee-Pour, H. Ghourchian and M. R. Gholami, *J. Mol. Catal. B: Enzym.*, 2011, 68, 206–210.
35. B. Liang, X. Guo, L. Fang, Y. Hu, G. Yang, Q. Zhu, J. Wei and X. Ye, *Electrochem. Commun.*, 2015, 50, 1–5.
36. Z. Li, C. Xie, J. Wang, A. Meng and F. Zhang, *Sens. Actuators, B*, 2015, 208, 505–511.
37. A. S. Campbell, Y. J. Jeong, S. M. Geier, R. R. Koepsel, A. J. Russell and M. F. Islam, *ACS Appl. Mater. Interfaces*, 2015, 7, 4056–4065.
38. K. H. Hyun, S. W. Han, W.-G. Koh and Y. Kwon, *J. Power Sources*, 2015, 286, 197–203.
39. E. Lavoron, *J. Electroanal. Chem. Interfacial Electrochem.*, 1974, 52, 395–402.
40. H. P. Peng, R. P. Liang, L. Zhang and J. D. Qiu, *Biosens. Bioelectron.*, 2013, 42, 293–299.