Polymeric Systems Containing Supramolecular Coordination Complexes for Drug Delivery

Feng Chen 1, Yang Li 1, Xiongjie Lin 1, Huayu Qiu 1,2,* and Shouchun Yin 1,*

1 College of Material, Chemistry and Chemical Engineering, Hangzhou Normal University, Hangzhou 311121, China; chenfeng@stu.hznu.edu.cn (F.C.); liyang@hznu.edu.cn (Y.L.); linxiongjie@stu.hznu.edu.cn (X.L.)
2 Key Laboratory of Organosilicon Chemistry and Materials Technology of Ministry of Education, Hangzhou Normal University, Hangzhou 311121, China
* Correspondence: hyqiu@hznu.edu.cn (H.Q.); yinsc@hznu.edu.cn (S.Y.)

Abstract: Cancer has become a common disease that seriously endangers human health and life. Up to now, the essential treatment method has been drug therapy, and drug delivery plays an important role in cancer therapy. To improve the efficiency of drug therapy, researchers are committed to improving drug delivery methods to enhance drug pharmacokinetics and cancer accumulation. Supramolecular coordination complexes (SCCs) with well-defined shapes and sizes are formed through the coordination between diverse functional organic ligands and metal ions, and they have emerged as potential components in drug delivery and cancer therapy. In particular, micelles or vesicles with the required biocompatibility and stability are synthesized using SCC-containing polymeric systems to develop novel carriers for drug delivery that possess combined properties and extended system tunability. In this study, the research status of SCC-containing polymeric systems as drug carriers and adjuvants for cancer treatment is reviewed, and a special focus is given to their design and preparation.

Keywords: supramolecular coordination complexes (SCCs); drug delivery; self-assembly; cancer therapeutics; polymeric systems

1. Introduction

Cancer is a growing health problem around the world, particularly with urbanization and subsequent changes in lifestyle and environmental conditions [1,2]. With the increasing global cancer burden, cancer treatment has become a major medical problem. In the past few decades, the improvements of diagnostic equipment and therapeutic technology have grown tremendously, and surgery, chemotherapy, and radiotherapy have become the three conventional methods of cancer treatment. At present, although most solid cancers can be surgically removed when the patient’s physical conditions allow, chemotherapy with high therapeutic efficiency is a necessary treatment for most cancers because cancer cells easily grow and expand. However, due to the small molecular size of simple cancer drugs, traditional chemotherapy has some limitations, such as poor biocompatibility, easy clearance by the blood or kidneys, no specific selectivity, low accumulation in cancerous tissues, and multidrug resistance. Photodynamic therapy is an excellent complement to chemotherapy due to its low toxicity, few side effects, less damage to normal tissues, and negligible drug resistance [3]. Unfortunately, most of the photosensitizer drugs are hydrophobic, and there are serious problems in transport and distribution in vivo. Therefore, how to develop a safe and effective drug delivery system is extremely urgent. Fortunately, with the development of nanomedicine, nanoparticle drug delivery systems have improved cancer treatment and can increase drug absorption, reduce side effects, and improve drug targeting [4]. In particular, the emergence of drug delivery systems based on polymeric systems is of great
significance in the field of biomedicine [5,6]. For example, amphiphilic copolymers containing both hydrophilic and hydrophobic chain segments can self-assemble into micelles with hydrophilic shells and hydrophobic cores at a certain concentration in solutions. Amphiphilic copolymers, with a unique core-shell structure, have promising applications in the transportation field of nanomedicine due to their advantages of high elasticity, excellent stability, and outstanding encapsulation [7–9].

In recent decades, supramolecular coordination complexes (SCCs) have rapidly developed and attracted considerable attention because of their well-defined sizes and shapes and wide applications [10–14]. For example, numerous two-dimensional (2D) metallacycles and three-dimensional (3D) metallacages with various functions have been synthesized through coordination-driven assemblies, and they have wide applications in catalysis, sensors, amphiphilic self-assembly, supramolecular polymers, host–guest chemistry, and drug delivery [15–27]. Moreover, SCC-based materials are potential candidates for drug delivery for the following reasons: first, the unique cavities of SCCs facilitate drug transport owing to the SCC’s hydrophobic property and adjustable size [28,29]. Second, the ingestion process of the drugs is realized by rationally designed SCC structures [30,31]. Third, ruthenium (Ru) or platinum (Pt) metals as the metal nodes of SCCs can be used as anticancer drugs or prodrugs owing to the anticancer activity of organometallic ruthenium or platinum complexes [32–36]. Moreover, SCCs, especially Pt(II)-based SCCs, enhance cellular uptake and bind to biomolecules with high affinity in vivo [37]. Compared with the current Pt(II) clinical drugs, Pt(II)-based SCCs can inhibit cancer growth, with lower toxicity to normal tissues, when used as cell-imaging agents and anticancer drugs. Fourth, captured drugs can be easily released because of the dynamic nature of the metal coordination bond of SCCs. Furthermore, SCCs will dissociate or change their configurations when they contact competitive ligands or when pH changes [38]. Finally, the integration of cancer diagnosis and treatment can be realized by introducing chromophores into SCCs [39–43].

The hydrophobic core of a polymeric nanoparticle is used as a drug-loading container to encapsulate hydrophobic compounds, and it is also an excellent choice for packaging hydrophobic SCCs to achieve the stability, solubility, and targeting ability of the encased SCCs in the physiological environment [44–46]. Then, the SCC-containing micelles work better in vivo under the protection of the hydrophilic shell to avoid being identified and devoured by the reticuloendothelial system. Additionally, given that the SCC structure can be easily modified, the hydrophilic groups or amphiphilic polymers can be used to decorate SCCs to build polymeric systems for biological applications. Interestingly, stimulus-responsive SCC-containing polymeric systems have also been developed for the controlled release of drugs. Nowadays, physical encapsulations by amphiphilic polymers and the chemical decoration of SCCs have become effective methods to fabricate polymeric drug delivery systems, and then polymeric systems containing SCCs with combined properties and extended system tunability open a novel window for drug delivery. Although the research on SCC-containing polymeric systems is still in infancy, a number of elegant studies have been reported. Herein, we try to give a systematic overview on the construction and anticancer properties of SCC-containing polymeric systems. We classify SCC-containing polymeric systems primarily depending on the synthetic strategy, including physical combination and chemical modification. We focus on the SCC-containing polymeric systems with synergistic treatment or the integration of cancer diagnosis and treatment in particular. Current challenges and future perspectives are also discussed.

2. SCCs Modified via Physical Combination with Amphiphilic Polymers

Polyethylene glycol (PEG) and amphiphilic polymers approved by the Food and Drug Administration, such as poly(ethyleneoxide)–poly(propylene oxide)–poly(ethylene oxide) (Pluronic F127) and distearoyl phosphoethanolamine–PEG (DSPE-PEG) are the most common excellent choices because of their commercialization and their capability to enhance the stability, solubility, and biocompatibility of theranostic and therapeutic agents [47–51]. Polymeric systems based on the physical combination of SCCs and amphiphilic polymers
can not only enhance the solubility and stability of a given SCC in aqueous media, but also exhibit a passive targeting effect on cancer tissues through the enhanced permeability and retention (EPR) effect [52,53]; the polymeric systems have been widely applied in drug delivery and cancer treatment, such as chemotherapy, cancer monitoring, and PDT.

Yu et al. synthesized a highly emissive platinum metallacage 1 as a component of therapeutic supramolecular nanoparticles, and mPEG-DSPE and biotin-PEG-DSPE were used to form nanoparticles 2 for adaptation to biological environment systems (Figure 1); then the metallacages were safely protected inside the hydrophobic interior [54]. In vitro and in vivo studies revealed that metallacage-loaded nanoparticles had higher anticervical cancer efficacy and lower toxicity than Pt(II) anticancer drugs such as oxaliplatin, carboplatin, and cisplatin. Importantly, tetraphenylethene, an aggregation-induced-emission luminogen, was introduced into the metallacage, resulting in strong radiation even at very low concentrations, which was suitable for biological imaging. In vivo fluorescence imaging demonstrated that nanoparticles showed superior fluorescence signals in cancers than in normal organs, confirming their diagnostic capabilities. This pioneering example of a metallacage-containing polymeric system provides an excellent nanoplatform on which to combine anticarcinogen with aggregation-induced-emission imaging and thus represents the blueprint for next-generation nanomedicines.

Efficient drug delivery carriers can improve the effect of chemotherapy. The delivery of drugs in an SCC-containing polymeric system is an efficient and relatively innovative method. In 2018, Zheng and others reported a Pt-drug delivery system based on Pt(IV) prodrugs, metallacages and amphiphilic polymers (Figure 2). They found that a well-defined host–guest interaction existed between the metallacage and fluorescein, in which fluorescein or its derivatives were encapsulated by the metallacage in a ratio of 1:1, with a μM dissociation constant ($K_d$) [55]. Moreover, the characteristic fluorescence and chromaticity changes of fluorescein were helpful for monitoring. Therefore, the authors designed and prepared a fluorescein-conjugated Pt(IV) prodrug 4, which was loaded into the metallacage through host–guest interaction. Then, an anionic block copolymer, methoxy PEG-block-polyglutamic acid, was incorporated to formulate the drug-loaded metallacages into nanoparticles with ideal charges and sizes (average size of 80 nm). All of the in vitro experiments showed that nanoparticles elegantly released Pt-therapeutics in the cervical cancer HeLa cells, and the therapeutic effect was comparable to that of cisplatin. This work demonstrated the use of SCC polymeric systems for Pt-drug encapsulation and delivery.

**Figure 1.** Representation of the formation of nanoparticles 2 from high emissive metallacages 1 and the mPEG-DSPE and biotin-PEG-DSPE. Scheme of the transportation and accumulation of nanoparticles 2 in tissue. Reproduced with permission from [54]. Copyright 2016, National Academy of Sciences (USA).
Photodynamic therapy is a new method of treating cancers using photosensitive drugs and visible-light activation. In PDT, the photosensitive drugs transfer energy to the surrounding oxygen, generating highly active $^1\text{O}_2$, which can oxidize nearby biological macromolecules and then generate cytotoxicity and kill cancer cells. Photodynamic therapy is an excellent supplement to chemotherapy because of its little drug resistance, minimal infiltration, fewer side effects, and less damage to marginal tissues [56–58]. Photosensitive drugs are important parts of PDT [59,60]. Among photosensitizers, porphyrin and its derivatives have attracted special attention for their excellent photophysical properties [61–63]. However, porphyrin derivatives show severe π–π stacking, due to their larger planar structures, which facilitates aggregation and therefore reduces their efficiency in generating active oxygen. To overcome these problems, SCCs for loading porphyrin and its derivatives or SCCs containing porphyrin groups have been designed [64–66] and then encapsulated by amphiphilic polymers to form nanoparticles and demonstrate excellent therapeutic effects.

Polymeric systems prepared using photosensitive SCCs and amphiphilic polymers have been reported successively. Yang’s group combined metallacycles and PEG-modified long-circulating liposome DSPE-mPEG to form metallacycle-containing nanoparticles for cancer treatment (Figure 3) [67]. The porphyrin-containing 120° donor and the diarylethene-containing diplatinum acceptor self-assembled into a discrete dual-stage metallacycle. Diarylethene was introduced into the metallacycle as a photochromic switch. When the diarylethene units were in their open-loop form 7, $^1\text{O}_2$ was efficiently generated by the porphyrin photosensitizer. In contrast, the formation of $^3\text{O}_2$ was severely inhibited when the diarylethene was converted to the closed-loop form 8, which was then reactivated and completely recovered by selective radiation at distinct wavelengths. The amphiphilic polymer mPEG-DSPE was used for the formation of nanoparticles, and two kinds of spherical micelles (9 and 10) with diameters of about 60 nm were obtained. These nanoparticles could deliver metallacycles to cervical cancer HeLa cells via endocytosis. The experimental evaluation showed that the $^1\text{O}_2$ generation efficiency of 9 was about 155 times that of 10, thus
In 2018, Yu et al. used 5,10,15,20-tetra(4-pyridyl)porphyrin (TPP) as one of the constituent elements and constructed a novel metallacage (Figure 4A). The intermolecular π–π stacking of TPP was effectively inhibited, resulting in a significant increase in fluorescence and $^{1}$O$_{2}$ quantum yield (the quantum yield value was 0.44, which was about 110 times that of TPP) [68], which is beneficial for PDT and near-infrared (NIR) fluorescence imaging. Metallacages PEGylated with mPEG-b-PEBP and RGD-PEG-b-PEBP endowed nanoparticles 10 with longer blood circulation time and less nonspecific cell uptake by the enhanced EPR effect and active targeting ability. Nanoparticles 10 possessed high photosensitivity because the energy gap between the lowest excited singlet state and the lowest excited triplet state of the metallacage was very small, which increased the rate of intersystem crossing and was conducive for $^{1}$O$_{2}$ generation. The doping of heavy atoms (Pt) into the metallacage further promoted the $^{1}$O$_{2}$ production, because Pt had a high spin-orbit coupling constant ($\chi = 4481$ cm$^{-1}$), which improved the rate of the rapid system crossing from singlet state to triplet state. Importantly, this system integrated chemotherapy and PDT on one platform, and both in vivo and in vitro experiments proved the excellent synergistic therapeutic effects of the system. In vitro, nanoparticles could effectively mediate 95.6% of cancer cell apoptosis and necrosis within 3 min of radiation. In vivo, after a single dose injection of the nanoparticle against U87MG, the cisplatin-resistant A2780CIS and orthotopic (4T1 and LM3) cancer models were significantly suppressed without metastasis and recurrence, and the life quality of mice was effectively improved and their life span was prolonged. In addition, based on the high affinity between porphyrin and metal ions, the use of $^{64}$Cu and paramagnetic Mn enabled the function of metallacage nanoparticles as imaging agents with deep tissue penetration; consequently, they could accurately diagnose cancers and monitor nanoparticle delivery, biodistribution, and excretion in real-time. Yu further reported the metallacage-based polymeric system as the photosen-
sitizer transport carrier [69]. The chemotherapeutic agents cis-(PET3)2Pt(OTf)2 (cPt) and hexakis[4-(4′-pyridylethynyl)phenyl]benzene (HPPB), a fluorophore, were assembled to form a dual-functionalized organic platinum(II) metallacage, which could form a complex with the photosensitizer octaethylporphyrin (OEP) through noncovalent interactions (Figure 4B). The further wrapping of metallacages with amphiphilic polymers via in situ copper-free click reaction endowed the cages with the function of specifically delivering OEP and cPt to ovarian cancer cells to overexpress α5β3 integrin. Benefitting from these reasonable designs, 15 has shown excellent anticancer properties in drug-resistant cancer models. These works have proved well that the delivery of photosensitizers through supramolecular chemistry provides a promising strategy for effective cancer treatment.

For photosensitizers, abundant photochemical and photophysical properties are essential. Ruthenium (II) complexes are good candidates for photosensitizers [34,70–72]. In 2019, Zhou and coworkers constructed a metallacage with Ru-Pt bimetal (Figure 5) [73]. Owing to the collection of multiple Ru(II) complexes and Pt(II) centers in a single supramolecular system, the metallacage became a high-efficiency photosensitizer with low side effects, showing a deep-red emission, a two-photon absorption cross-section, and a high active-oxygen generation efficiency after being activated under two-photon light irradiation. The nanoparticles formed by encapsulating metallacages with amphiphilic polymers were nontoxic and exhibited selective accumulation in lysosomes when they entered into cancer cells of A549 cancer bearing mice. In particular, two-photon excitation showed greater penetration depth than one-photon excitation, resulting in lower dark cytotoxicity and higher cytotoxicity when photosensitizers were activated by two-photon irradiation, proving the excellent PDT performance of nanoparticles.

In previous studies [74–79], polymeric systems composed of SCC-loaded amphiphilic polymers and fluorophores with emission in the second near-infrared window (NIR-II) have been found to play an important role in cancer therapy. As shown in Figure 6A, Kim and colleagues used Pluronic F127 to encapsulate their Pt(II)-based metallacycle 20 and NIR-II molecular dye 21 to obtain a novel NIR-II nano-theranostic agent 22 [80]. After F127 encapsulation, the encapsulated nanoparticles 22 were discrete and uniform, with an average size of about 110 nm; they not only exhibited excellent solubility and biocompatibility but also enabled higher priority accumulation at the cancer site than 20 and 21. The cocktail based on the platform 22 demonstrated its potential as a multifunctional
platform. Metallacycle 20 in 22 was internalized into glioma U87MG cells and exhibited no significant internalization effect in noncancerous tissues, which suggested that 22 reduced the systemic toxicity of Pt(II)-based drugs to normal tissues and organs. Additionally, the encapsulation efficiency of 21 in 22 was 87.4 ± 1.7%. Nanoparticles 22 displayed bright fluorescence in the NIR-II region, and the fluorescence did not show any significant change upon short- and long-term irradiation in different media, which indicated that the encapsulated 21 endowed 22 with good optical properties and favorable photo-stability. Thus, the blood circulation system was visualized and the glioma was accurately located with high resolution. This nanoplatform offers a potential strategy for glioma treatment by transporting SCCs and NIR-II fluorophores with diagnostic and therapeutic functions.

![Figure 5.](image)

**Figure 5.** (A) Preparation of nanoparticles 19 formed by encapsulating metallacages 18 with amphiphilic polymers and their application in two-photon PDT. (B) Cancer growth inhibition curves of A549 for different treatments. (C) Body weights of mice during different treatments. Reproduced with permission from [73]. Copyright 2019, National Academy of Sciences (USA).

Furthermore, highly biocompatible and water-soluble melanin biopolymers have been actively explored for use in drug delivery systems [81–84]. Compared with traditional amphiphilic polymers as carriers, melanin dots can not only load more drugs through π–π stacking but also absorb NIR optical energy and convert it into heat energy for photothermal therapy (PTT). The heat released by the melanin dots can stimulate the sound waves in the surrounding medium and finally convert them into photoacoustic signals; this property makes the melanin dots a suitable tool for pretreatment imaging guidance. In 2019, Sun et al. reported the melanin-dot-mediated drug delivery system of SCCs for NIR-II/photoacoustic dual-modal imaging-guided chemo-photothermal synergistic therapy [85]. The authors designed and synthesized a multifunctional therapeutic agent 25 based on molecular-dye-modified melanin dots and rhomboidal Pt(II) metallacycles 23; the therapeutic agent showed excellent optical properties and passive targeting ability for U87MG cancers (Figure 6B). The photoacoustic imaging of melanin dots and the NIR-II fluorescence imaging of molecular dyes were compatible in nanoagent 25, and nanoagent 25 had a higher priority passive accumulation in the cancer site through the EPR effect, so that the treatment process was accurately guided and the evaluation of the treatment effect was accurate. Importantly, the combination of the anticancer activity of Pt(II) metallacycles 23 and the photothermal properties of melanin dots enabled the realization of synergistic PTT. The results showed that PTT combined with chemotherapy could significantly reduce the drug resistance and cancer recurrence under the guidance of intrinsic signal feedback from the therapeutic agents. These results provide an opportunity for the design of novel therapeutic drugs, which can be used in the NIR-II region for biomedical applications.
3. SCCs Decorated via Chemical Modification with Amphiphilic Polymers

Compared with the physical encapsulation of SCCs by amphiphilic polymers for drug transport, chemical modification is a more direct and effective means to apply SCCs to biological systems [86]. The external functionalization of SCCs increases the diameter, enables nanoparticles to exhibit the EPR effect, and allows the loading of other drugs into the polymeric scaffold, which can result in better assisted or synergizing therapy. Tang reported the advantages of functionalized metallacycles with a hydrophilic compound [87]. A series of metallacycles with porphyrin were designed and synthesized, among which metallacycles 26 and 27 were tailed by diol chains, while metallacycle 28 had no hydrophilic part (Figure 7). As a result of hydrophobic and hydrophilic interactions, amphiphilic metallacycles 26 and 27 self-assembled into micelles with ∼100 nm diameter in aqueous solution and effectively entered the cells. However, metallacycle 28 could not form micelles because of its complete hydrophobicity; thus, it only passively diffused into the cells. Therefore, metallacycles 26 and 27 micelles exhibited remarkably enhanced cell uptake and anticancer efficiency. This study visually demonstrates the necessity of chemical modification for the application of SCCs in biological systems.

Figure 7. Structure of metallacycles 26 and 27 tailed by diol chains and metallacycle 28 without hydrophilic part. Reproduced with permission from [87]. Copyright 2018, The Royal Society of Chemistry.

The direct introduction of hydrophilic groups into SCCs is generally considered an excellent approach to form nanoparticles. The synthetic modification of the ligand incorporated into a glycosyl group endows SCCs with amphiphilicity and helps to improve the water solubility of SCCs. As shown in Figure 8, Yin et al. successfully constructed an amphiphilic metallacycle 29 modified by glucose groups; the metallacycle self-assembled to

Figure 6. (A) Synthesis of the nanoparticle 22 from metallacycle 20, NIR-II molecular dye 21, and Pluronic F127. Reproduced with permission from [80]. Copyright 2019, The Royal Society of Chemistry. (B) Structures of discrete rhomboidal Pt(II) 23 and NIR-II molecule 24. Representation of the formation of 25 and the cellular uptake of rhomboid 23 from nanoparticles. Reproduced with permission from [85]. Copyright 2019, National Academy of Sciences (USA).
form micelles, driven by hydrophilic and hydrophobic interactions at the concentration of $2.5 \times 10^{-4} \text{ M}$ in water [88]. Then, the micelles became a drug carrier for neutral doxorubicin (DOX) and provided a drug delivery system 31, whose DOX-loading capacity was 10.5%. Experiments have demonstrated that these nanocarriers effectively delivered DOX into U87 cancer cells through endocytosis and released DOX into the cell nucleus because of the cancer cell acidic environment. Micelle 31 not only overcame the large toxic and side effects of DOX on normal tissues but also improved the therapeutic effect of neuroglioma, due to the simultaneous existence of Pt(II) and DOX. This study provides a potential strategy to synthesize pH-responsive amphiphilic metallacycles as carriers for drug delivery and cancer treatment.

![Formation of nanomicelles 30 via self-assembly of amphipathic metallacycles 29, and illustration of the cellular uptake of micelle 31 and DOX release from 31. Reproduced with permission from [88]. Copyright 2020, American Chemical Society.](image)

Besides simple hydrophilic groups, PEG is also used to chemically modify SCCs, due to its hydrophilicity and convenient preparation. Then, the polymeric systems constructed using amphiphilic SCCs are applied in drug delivery because of their cavity structure or other characteristics. In 2011, Zhou and colleagues functionalized the surface of alkyne-covered metallacages through a click reaction with azide-terminated PEG to obtain a PEGylated alkyne-decorated copper cage, and a good balance between solubility and effective molecular stacking was achieved (Figure 9A) [89]. The anticancer drug 5-fluorouracil could enter the metallacage cavity through Lewis base interactions, and its loading capacity was 4.38 wt%, while that of the drug encapsulated in pure PEG was only 0.82 wt%. Importantly, the system loaded with 5-fluorouracil showed controlled release after dialysis in PBS buffer (pH = 7.4) for 24 h. This work opened a window toward the postsynthesis modification of SCCs to construct a polymeric system for drug delivery.

Additionally, PEG-modified metallacycles were used for drug delivery via host–guest interaction. Cucurbit[n]uril (CB[n]) ($n = 5–8, 10,$ and 14) is a family of barrel-shaped macrocyclic molecules composed of repeated glycoluril units [90–92]. Various neutral or positively charged guests can be encapsulated in cavities with a high equilibrium association constant. In previous studies, a host–guest complex composed of water-soluble metallacage and CB8 was used as a carrier to transport curcumin (Cur) [93] into cancer cells [94]. The pyridine donor containing methyl viologen (MV) units and the organoplatinum acceptor containing the tri(ethylene glycol) group were assembled into a water-soluble metallacage. The MV units on the metallacycles were incorporated with three equivalents of CB8, and the resulting complex further encapsulated 1.5 equivalent of Cur via heteroternary host–guest complex formation (Figure 9C). Depending on different concentrations, Cur-embedded
heteroternary complex exhibited various morphological features, such as cellular networks, fibers, and vesicles. The Cur-embedded heteroternary complex in different cancer cell lines all showed good anticancer activities. The growth inhibition efficiencies on human melanoma (C32), rodent melanoma (B16F10), and hormone-responsive (MCF-7) and triple-negative (MDA-MB231) breast cancer cells were significantly higher than those of free Cur, and the IC50 value was reduced to the biologically significant level of \( p < 0.0001 \). Therefore, this work solved the limitations of curcumin as an anticancer drug with poor absorption, low water solubility, and low bioavailability for rapid metabolism.

![Figure 9](image_url)

**Figure 9.** (A) Synthesis of metallacage 33 from metallacage 32 through click reaction. (B) The release of 5-fluorouracil from control (square) and cage 33 (circle). Reproduced with permission from [89]. Copyright 2010, John Wiley and Sons. (C) Illustration of the formation of host–guest complex 36 from the self-assembly of 34, CB8, and curcumin (Cur). (D) IC50 of each component in different cells. Reproduced with permission from [94]. Copyright 2018, National Academy of Sciences (USA).

Dendrimers [95–97], a type of polymer, have become a basic building block for the manufacture of functional nanoscale systems. The characteristics of dendrimers and the dynamic properties of supramolecular metallacycles are combined to obtain supramolecular metallobimolecular dendrimers [98]. These supramolecular metallobimolecular dendrimers have huge potential for the extraction, storage, and release of compounds (such as drugs) for the final nanosstructures. One example of dendritic metallacyle-cored nanoparticles was reported by Chen et al. in 2014 [99]. The metallacyle had peripherally dimethyl isophthalate functionalized poly(benzyl ether) dendrites and self-assembled into ordered nanostructures via the orthogonality of metal–ligand coordination and other weak interactions (including π–π stacking, CH–π interaction, and atypical hydrogen bonds). The nanoscale vesicles were assembled from discrete metallacycles 37–39, and their sizes were relatively monodisperse. Metallobimolecular dendrimer 39 was successfully assembled into nanoparticles with an average size of 100–200 nm and with the capability of loading fluorescent dyes, such as boron dipyrromethene and sulforhodamine B (Figure 10). Owing to the kinetic properties of the metal–ligand bonds, the decomposition and reassembly of the obtained hexagonal metallobimolecular dendrimers were reversibly controlled by adding or removing bromine ions. The vesicles formed by 39 were destroyed and transformed into micelles and successfully released fluorescent dyes. This nanostructure enriched the structural types of SCCs, and it has the potential to be used as a nanocapsule for guest encapsulation and controlled release.
Figure 10. Structure of metalloendritic hexagons 37-39. Illustration of the formation of nanoparticles 40 from the self-assembly of 39 and the process of halide-responsive release of fluorescent molecules. Reproduced with permission from [99]. Copyright 2014, American Chemical Society.

Polymerizing independent SCCs through an appropriate chemical reaction is also a simple and efficient method to obtain an SCC-based polymeric system, which is an alternative approach for SCC postmodification. In 2016, Zhang and colleagues reported fluorescent polymers synthesized via the covalent linkage of TPE-based metallacycles for bioimaging [39]. Specifically, the metallacycle was prepared through the reaction of exposed amino groups with N-hydroxysuccinimide-activated carboxylic acids in a mild, efficient, and uncatalyzed amidation reaction to synthesize polymers 42 and 43 (Figure 11). Then, the polymers were further prepared at low concentrations into nanoparticles for application in biological systems. Because of the aggregation-induced-emission characteristics of tetr phenylvinyl donors and the aggregation of the metallacycles by polymerization, these polymers exhibited strong emissions and excellent quantum yields and thus have the potential to act as useful cell-imaging agents. Indeed, nanoparticles were significantly more enriched in the lungs than in other organs, as determined through the research on images and fluorescence counts of different organs after the intravenous injection of 43. Therefore, based on the anticancer activity of the Pt(II) SCCs, these metallacycle-cored polymers could serve as theranostic agents for both cell imaging and lung cancer therapy.

The above-mentioned drug delivery systems are all traditional amphiphilic polymeric systems, and novel supra-amphiphilic polymeric systems are developed rapidly. In contrast to conventional amphiphiles, supra-amphiphiles are constructed based on noncovalent interactions or dynamic covalent bonds [100,101]. The development of supra-amphiphiles not only enriches the family of amphiphiles but also offers a new kind of building block for the preparation of complex self-assemblies. Similarly, the polymeric systems formed by supra-amphiphilic SCCs provide more possibilities for drug transportation. For example, in 2016, Isaacs and coworkers developed a Fujita-type cuboctahedral Pd(II) metallacage consisting of methyl viologen, and it was further noncovalently functionalized with CB8 [102]. Then, a kind of DOX prodrug was synthesized using 2-alkoxynaphthalene, which had a high affinity to CB8 and was successfully encapsulated by supra-amphiphilic metallacage via host–guest interaction (Figure 12A). The DOX prodrug was successfully delivered into cervical cancer HeLa cells, and it leveraged the acid-sensitive acylhydrazone linkage and released free DOX from the nanoparticles in the acidic cancer cell environment. The cytotoxicity of this system was comparable to that of free DOX, and the system showed significantly higher potency to HeLa cells (IC50 = 48 ± 8 nm). This work demonstrates the
potential of supra-amphiphilic polymeric systems for high drug uptake, targeted delivery, and selective release.

Figure 11. (A) Synthetic routes of metallacycle 41 and polymers 42 and 43. (B) Images of a mouse and organs after an intratumoral injection of 43. Reproduced with permission from [39]. Copyright 2016, National Academy of Sciences (USA).

Figure 12. (A) Representation of self-assembly of methyl viologen 44 as first guest with CB8 to yield metallacage 45 followed by heteroternary complex formation with 2,6-dihydroxynaphthalene (HN) or DOX prodrug to yield 46 and 47. Reproduced with permission from [102]. Copyright 2016, American Chemical Society. (B) Schematic illustration of the chemical-responsive release of DOX or Nile Red from the hydrophobic cavity of 48 via chemical stimulus with adamantane ammonium. Reproduced with permission from [103]. Copyright 2017, American Chemical Society.

Metallacage 45, which was noncovalently decorated with CB[n], was less robust for in vivo applications due to its potential for dissociation. In 2017, Isaacs and coworkers...
reported a supra-amphiphilic metallacage with mechanically interlocked architecture [103]. In this improved system, Pd$_{12}$L$_{24}$ metallacage was covalently bonded with CB7 and embedded with long hydrophobic carbon chains. The hydrophobic environment was produced by the complexing of CB7 units with functionalized alkanediammonium ions on the hydrophobic tails, and it could take up DOX or Nile Red. The addition of competing guest adamantane amine, which bound with the CB7, caused the release of DOX or Nile Red (Figure 12B). Owing to the multiplicity of CB7 units on the metallacage surface, this functional uptake and release system showed a promising supra-amphiphilic platform to enable diagnostic and therapeutic applications.

4. SCCs Modified by Stimulus-Responsive Amphiphilic Polymers

Stimulus-responsive polymers are polymers that exhibit significant changes in physical or chemical properties when exposed to small environmental stimuli. Because of their unique properties, they are usually used as smart materials in drug delivery, diagnosis, tissue engineering, intelligent and optical systems, and biosensors [104,105]. The SCC modification by amphiphilic polymers responsive to multiple stimuli not only allows the SCCs to smoothly self-assemble into micelles but also improves the drug-release controllability.

In biological systems, the glutathione (GSH) contents of intracellular and extracellular environments are different, and the GSH content is higher in cancer cells. Considering this, in 2017, Stang and colleagues modified the aggregation-induced luminescence metallacycle with amphiphilic polymer and introduced a GSH-responsive group into the polymer backbone, which allowed the stimulation-controlled release of the drugs (Figure 13A) [40]. The metallacycle-based polymer was further self-assembled into 50 nm (51) and 500 nm (52) nanoparticles and 0.8–3.0 μm vesicles (53) through reprecipitation, dialysis, and double emulsification technology. The brush-like PEG chains on the surface of the nanostructures prevented nanoparticles from being adsorbed by proteins and removed by the reticuloendothelial system; this provides these nanostructures a better chance to exude from the cancer blood vessels. Among nanoparticles 51 and 52 and vesicles 53, nanoparticles 51 exhibited high cancer accumulation and excellent cancer-penetration ability, increased uptake by cervical cancer HeLa cells, prolonged circulation half-life, presented a relatively long blood circulation time, and reduced IC$_{50}$ value. In addition, the hydrophobic cores of 51 and 52 were suitable platforms for loading neutral DOX, and the hollow cavity of 53 could encapsulate doxorubicin hydrochloride to form a dual drug system of Pt(II) and DOX. Metallacycle-based nanoparticles or vesicles were disassembled via a GSH-triggered cascade elimination of protection polymer, and then, the encapsulated DOX or doxorubicin hydrochloride was released. After 4 h of treatment, the metallacycle fluorescence and the red fluorescence of DOX were observed in the cytoplasm. After 24 h, GSH triggered the successful release of the loaded DOX. The calculated anticancer index of 51 loaded with DOX was 0.79, indicating a good synergistic anticancer effect. These experiments were performed using other similar hydrophobic drugs such as paclitaxel instead of DOX, and similar results were obtained.

In 2020, Stang and colleagues reported a new work in which the amphiphilic supramolecular block copolymer 54 was composed of a well-defined metallacyle core and H$_2$O$_2$-reactive diblock copolymers arms; it was self-assembled into nanoparticles 55 (Figure 13E) [106]. The presence of the metallacyle reduced the critical aggregation concentration to 4.94 μg/mL from 40.3 μg/mL. The nanoparticles could encapsulate DOX and palmitoyl ascorbate (PA). The best PA/DOX ratio was 1:4, which had the best anticancer effect. In cancer tissues, PA served as a pro-oxidant to increase the H$_2$O$_2$ concentration in the cell through the cascade elimination reaction, which broke the hydrophobic protective group, thereby achieving the reversion of the amphiphilic nature of copolymer 25 and leading to the destruction of the nanostructure and the subsequent release of the drug. Benefiting from the EPR effect, the amount of DOX in the cancer gradually increased to 5.7 ± 0.8% ID/g after treatment with 55 by 12 h injection, and the DOX amount in the cancer remained at a high level (5.5 ± 0.7% ID/g) even at 24 h postinjection, which contributed to the anticancer
performance. This work illustrated the potential of metallacycle-based polymeric systems for synergistic anticancer applications through chemotherapy and oxidative stress.

Figure 13. (A) Structure of metallacycle 50. (B) Illustration of synthesis of nanoparticles 51 and 52 and vesicles 53 and their GSH-triggered amphiphilicity reversion mechanism. (C) Blood circulation time of 51, 52, DOX·HCl, and cisplatin after IV injection into normal mice. (D) Cancer growth inhibition curve for 25 day injection (NP3 are micelles without the cage center). Reproduced with permission from [40]. Copyright 2017, American Chemical Society. (E) Schematic representation of H2O2-responsive diblock copolymers arms; it was self-assembled into nanoparticles pramolecular block copolymer in the cytoplasm. After 24 h, GSH triggered the successful release of the loaded DOX. The drugs such as paclitaxel instead of DOX, and similar results were obtained. Then, the encapsulated DOX or doxorubicin hydrochloride was released. After 4 h of were disassembled via a GSH-triggered cascade elimination of protection polymer, and form a dual drug system of Pt(II) and DOX. Metallacycle-based nanoparticles or vesicles in the cancer remained at a high level (5.5 ± 0.7% ID/g) even at 24 h postinjection, which chance to exude from the cancer blood vessels. Among nanoparticles the nanostructures prevented nanoparticles from being adsorbed by proteins and re-

5. Perspectives and Challenges

The practicability of SCC-containing polymeric systems in various cancer treatments is demonstrated obviously from the many examples presented. On one hand, a strategy is provided from SCC-containing polymeric systems to effectively solve the problems of poorly water-soluble, low cancer selectivity, and high toxicity of hydrophobic anticancer drugs and platinum-based anticancer drugs. Thus, a blueprint for the preparation of next-generation anticancer drug vehicles is urgently needed. On the other hand, the construction and anticancer properties of SCC-containing polymeric systems promote the development of novel cancer therapy methods that include PDT, photothermal therapy and immunotherapy, as well as synergistic therapy. Nevertheless, the research in this field is still in the early stage. The drug-loading rate of the SCC-containing polymeric system is not high enough, and the kinds of loaded drugs are limited; they mainly include cisplatin, DOX, 5-fluorouracil, and other hydrophobic drugs. Thus, how to use molecular design to improve the drug-loading efficiency and expand the types of drug transportation is worth considering. Moreover, the influence of the size of the SCC on cytotoxicity and metabolic mechanisms is still unclear, and the clinical practicability of SCCs must be further explored.

The characteristics of SCC-containing polymeric systems are affected by the chemical properties of building blocks and the geometry of their linkages. For example, on the basis of metallacage 11, the use of 64Cu and paramagnetic Mn enabled the function of metallacage nanoparticles as imaging agents with deep tissue penetration [68]. Therefore, we suggest more attention be paid to the basic structural construction of the SCC-containing polymeric system, including the introduction of various polymers with stimulus responsiveness and the integration of multifunctional ligands and so on, to overcome the current limitations and bring new opportunities for practical uses. With the continuous expansion of the related structure library, attractive SCC-containing polymeric systems can constantly be developed. For instance, SCC-containing polymeric systems have significant prospects for encapsulating hydrophilic proteins, even small interfering RNA through appropriate design of their structure.
6. Conclusions

This review presents the research progress of SCCs perfectly combined with amphiphilic polymers or hydrophilic groups either physically or chemically, presenting the diversity of SCC-containing polymeric systems. We have described a SCC-containing polymeric system with excellent solubility, stability, and biocompatibility as a promising component of cancer therapy. In drug delivery systems, SCC-containing polymeric systems not only substantially use their cavity structure to load various drugs, but they also intelligently utilize noncovalent interaction or stimulus responsiveness to achieve targeted delivery and controlled release. In cancer therapy, Pt(II) SCC-containing polymeric systems are usually used for chemotherapy, ROS-generating SCC-containing polymeric systems are used for PDT, and SCC-containing polymeric systems with aggregation-induced emission effect or NIR-II imaging technology are directly used for cancer diagnosis and therapy. Importantly, diagnosis and synergetic treatment are integrated in a single platform by introducing diverse functional organic units in SCCs, and then the conjugation of therapies significantly improves the therapeutic effect. Exploration of the utility of these SCC-containing polymeric systems for cancer therapy is still ongoing, and the possibility of curing cancer and embracing a better life is foreseen.

Although multifunctional SCC-polymeric systems represent a new class of promising biomedical materials with numerous possibilities, the vigorous future of this field requires continuous effort from individuals with different backgrounds. We expect this review to be attractive to researchers, and that it may arouse new interest and bring new opportunities for the development of SCC-containing polymeric systems.

Author Contributions: S.Y. and H.Q. initiated the work upon the invitation, designed the proposal and revised the manuscript. F.C. and Y.L. wrote the first draft of the manuscript. X.L. prepared the figures. All authors have read and agreed to the published version of the manuscript.

Funding: This research was funded by the National Natural Science Foundation of China (Grant Nos. 21971049 and 51903070).

Acknowledgments: The authors thank the College of Material, Chemistry and Chemical Engineering, Hangzhou Normal University, for equipment support.

Conflicts of Interest: The authors declare no conflict of interest.

References

1. Siegel, R.L.; Miller, K.D.; Jemal, A. Cancer Statistics, 2020. CA Cancer J. Clin. 2020, 70, 7–30. [CrossRef] [PubMed]
2. Feng, R.-M.; Zong, Y.-N.; Cao, S.-M.; Xu, R.-H. Current Cancer Situation in China: Good or Bad News from the 2018 Global Cancer Statistics? Cancer Commun. 2019, 39, 22. [CrossRef] [PubMed]
3. Dougherty, T.J.; Gomer, C.J.; Henderson, B.W.; Jori, G.; Kessel, D.; Korbelik, M.; Moan, J.; Peng, Q. Photodynamic Therapy. J. Natl. Cancer Inst. 1998, 90, 889–905. [CrossRef] [PubMed]
4. Chen, H.; Gu, Z.; An, H.; Chen, C.; Chen, J.; Cui, R.; Chen, S.; Chen, W.; Chen, X.; Chen, X.; et al. Precise Nanomedicine for Intelligent Therapy of Cancer. Sci. China Chem. 2018, 61, 1503–1552.
5. Nicolas, J.; Mura, S.; Brambilla, D.; Mackiewicz, N.; Couvreur, P. Design, Functionalization Strategies and Biomedical Applications of Targeted Biodegradable/Biocompatible Polymer-Based Nanocarriers for Drug Delivery. Chem. Soc. Rev. 2013, 42, 1147–1235. [CrossRef]
6. Fox, M.E.; Szoka, F.C.; Fréchet, J.M.J. Soluble Polymer Carriers for the Treatment of Cancer: The Importance of Molecular Architecture. Accounts Chem. Res. 2009, 42, 1141–1151. [CrossRef]
7. Pottanam Chali, S.; Ravoo, B.J. Polymer Nanocontainers for Intracellular Delivery. Angew. Chem. Int. Ed. 2020, 59, 2962–2972. [CrossRef]
8. Palivan, C.G.; Goers, R.; Najer, A.; Zhang, X.; Car, A.; Meier, W. Bioinspired Polymer Vesicles and Membranes for Biological and Medical Applications. Chem. Soc. Rev. 2016, 45, 377–411. [CrossRef]
9. Szafraniec-Szcieszny, J.; Janik-Hazuka, M.; Odrobińska, J.; Zapotoczny, S. Polymer Capsules with Hydrophobic Liquid Cores as Functional Nanocarriers. Polymers 2020, 12, 1999. [CrossRef]
10. Cook, T.R.; Stang, P.J. Recent Developments in the Preparation and Chemistry of Metallacycles and Metallacages via Coordination. Chem. Rev. 2015, 115, 7001–7045. [CrossRef]
11. Cook, T.R.; Zheng, Y.-R.; Stang, P.J. Metal–Organic Frameworks and Self-Assembled Supramolecular Coordination Complexes: Comparing and Contrasting the Design, Synthesis, and Functionality of Metal–Organic Materials. Chem. Rev. 2013, 113, 734–777. [CrossRef] [PubMed]
12. Chakrabarty, R.; Mukherjee, P.S.; Stang, P.J. Supramolecular Coordination: Self-Assembly of Finite Two- and Three-Dimensional Ensembles. *Chem. Rev.* 2011, 111, 6810–6918. [CrossRef] [PubMed]

13. Smulders, M.M.J.; Riddell, I.A.; Browne, C.; Nitschke, J.R. Building on Architectural Principles for Three-Dimensional Metallo-supramolecular Construction. *Chem. Soc. Rev.* 2013, 42, 1728–1754. [CrossRef] [PubMed]

14. Seidel, S.R.; Stang, P.J. High-Symmetry Coordination Cages via Self-Assembly. *Accounts Chem. Res.* 2002, 35, 972–983. [CrossRef] [PubMed]

15. Judge, N.; Wang, L.; Ho, Y.Y.L.; Wang, Y. Molecular Engineering of Metal-Organic Cycles/Cages for Drug Delivery. *Macromol. Res.* 2018, 26, 1074–1084. [CrossRef]

16. Sepehrpour, H.; Fu, W.; Sun, Y.; Stang, P.J. Biomedically Relevant Self-Assembled Metallacycles and Metallacages. *J. Am. Chem. Soc.* 2019, 141, 14005–14020. [CrossRef] [PubMed]

17. Sun, Y.; Chen, C.; Stang, P.J. Soft Materials with Diverse Suprastructures via the Self-Assembly of Metal–Organic Complexes. *Accounts Chem. Res.* 2019, 52, 802–817. [CrossRef] [PubMed]

18. Li, B.; He, T.; Fan, Y.; Yuan, X.; Qiu, H.; Yin, S. Recent Developments in the Construction of Metallacycle/Metallacage-Cored Supramolecular Polymers via Hierarchical Self-Assembly. *Chem. Commun.* 2019, 55, 8036–8059. [CrossRef] [PubMed]

19. Li, Y.; Zhang, J.; Li, H.; Fan, Y.; He, T.; Qiu, H.; Yin, S. Metallacycle/Metallacage-Cored Fluorescent Supramolecular Assemblies with Aggregation-Induced Emission Properties. *Adv. Opt. Mater.* 2020, 8, 1902190. [CrossRef]

20. Yoshizawa, M.; Klosterman, J.K.; Fujita, M. Functional Molecular Flasks: New Properties and Reactions within Discrete, Self-Assembled Hosts. *Angew. Chem. Int. Ed.* 2009, 48, 3418–3438. [CrossRef]

21. Vardhan, H.; Yusubov, M.; Verpoort, F. Self-Assembled Metal–Organic Polyhedra: An Overview of Various Applications. *Coord. Chem. Rev.* 2016, 306, 171–194. [CrossRef]

22. Zhang, Q.; Tang, D.; Zhang, J.; Ni, R.; Xu, L.; He, T.; Lin, X.; Li, X.; Qiu, H.; Yin, S.; et al. Self-Healing Heterometallic Supramolecular Polymers Constructed by Hierarchical Assembly of Triply Orthogonal Interactions with Tunable Photophysical Properties. *J. Am. Chem. Soc.* 2019, 141, 17909–17917. [CrossRef] [PubMed]

23. Lu, C.; Zhang, M.; Tang, D.; Yan, X.; Zhang, Z.; Zhou, Z.; Song, B.; Wang, H.; Li, X.; Yin, S.; et al. Fluorescent Metallacage-Core Supramolecular Gel Formed by Orthogonal Metal Coordination and Host–Guest Interactions. *J. Am. Chem. Soc.* 2018, 140, 7674–7680. [CrossRef] [PubMed]

24. Xu, L.; Shen, X.; Zhou, Z.; He, T.; Zhang, J.; Qiu, H.; Saha, M.L.; Yin, S.; Stang, P.J. Metallacycle-Cored Supramolecular Polymers: Fluorescence Tuning by Variation of Substituents. *J. Am. Chem. Soc.* 2018, 140, 16920–16924. [CrossRef] [PubMed]

25. Ahmad, N.; Younus, H.A.; Chughtai, A.H.; Verpoort, F. Metal–Organic Molecular Cages: Applications of Biochemical Implications. *Chem. Soc. Rev.* 2015, 44, 9–25. [CrossRef] [PubMed]

26. Casini, A.; Woods, B.; Wenzel, M. The Promise of Self-Assembled 3D Supramolecular Coordination Complexes for Biomedical Applications. *Inorg. Chem.* 2017, 56, 14715–14729. [CrossRef]

27. Li, Z.; Yan, X.; Huang, F.; Sepehrpour, H.; Stang, P.J. Near-Infrared Emissive Discrete Platinum(II) Metallacycles: Synthesis and Application in Ammonia Detection. *Org. Lett.* 2017, 19, 5728–5731. [CrossRef]

28. Xu, W-Q.; Fan, Y-Z.; Wang, H-P.; Teng, J.; Li, Y-H.; Chen, C-X.; Fenske, D.; Jiang, J-J.; Su, C-Y. Investigation of Binding Behavior between Drug Molecule 5-Fluoracil and M4L4-Type Tetrahedral Cages: Selectivity, Capture, and Release. *Chem. Eur. J.* 2017, 23, 3542–3547. [CrossRef]

29. Kaiser, F.; Schmidt, A.; Heydenreuter, W.; Altmann, P.J.; Casini, A.; Sieber, S.A.; Kühn, F.E. Self-Assembled Palladium and Platinum Coordination Cages: Photophysical Properties and Anticancer Activity. *Eur. J. Inorg. Chem.* 2016, 5189–5196. [CrossRef]

30. Preston, D.; Lewis, J.E.M.; Crowley, J.D. Multicavity [PdnL4]2n+ Cages with Controlled Segregated Binding of Different Guests. *J. Am. Chem. Soc.* 2017, 139, 2379–2386. [CrossRef]

31. Zheng, Y-R.; Suntharalingam, K.; Johnstone, T.C.; Lippard, S.J. Encapsulation of Pt(IV) Prodrugs within a Pt(II) Cage for Drug Delivery. *Chem. Sci.* 2015, 6, 1189–1198. [CrossRef]

32. Dubey, A.; Jeong, Y.J.; Jo, J-H.; Woo, S.; Kim, D.H.; Kim, H.; Kang, S.C.; Stang, P.J.; Chi, K-W. Anticancer Activity and Autophagy Involvement of Self-Assembled Arene–Ruthenium Metallacycles. *Organometallics* 2015, 34, 4507–4514. [CrossRef]

33. Mishra, A.; Jeong, Y.J.; Jo, J-H.; Kang, S.C.; Lah, M.S.; Chi, K-W. Anticancer Potency Studies of Coordination Driven Self-Assembled Arene–Ru-Based Metalla-Bowls. *ChemBioChem* 2014, 15, 695–700. [CrossRef] [PubMed]

34. Zeng, L.; Gupta, P.; Chen, Y.; Wang, E.; Ji, L.; Chao, H.; Chen, Z-S. The Development of Anticancer Ruthenium(II) Complexes: From Single Molecule Compounds to Nanomaterials. *Chem. Soc. Rev.* 2017, 46, 5771–5804. [CrossRef]

35. Zhang, X.; Liu, D.; Lv, F.; Yu, B.; Shen, Y.; Cong, H. Recent Advances in Ruthenium and Platinum Based Supramolecular Coordination Complexes for Antitumor Therapy. *Colloids Surf. B* 2019, 182, 110373. [CrossRef] [PubMed]

36. Rosenberg, B.; Vancamp, L.; Troscio, J.E.; Mansour, V.H. Platinum Compounds: A New Class of Potent Antitumour Agents. *Nature* 1969, 222, 385–386. [CrossRef]

37. Jana, A.; Bhowmick, S.; Kumar, S.; Singh, K.; Garg, P.; Das, N. Self-Assembly of Pt(II) Based Nanoscale Ionic Hexagons and Their Anticancer Potencies. *Inorg. Chim. Acta* 2019, 484, 19–26. [CrossRef]

38. McConnell, A.J.; Wood, C.S.; Neelakandan, P.P.; Nitschke, J.R. Stimuli-Responsive Metal–Ligand Assemblies. *Chem. Rev.* 2015, 115, 7729–7793. [CrossRef]

39. Zhang, M.; Li, S.; Yan, X.; Zhou, Z.; Saha, M.L.; Wang, Y-C.; Stang, P.J. Fluorescent Metallacycle-Cored Polymers via Covalent Linkage and Their Use as Contrast Agents for Cell Imaging. *Proc. Natl. Acad. Sci. USA* 2016, 113, 1100–1105. [CrossRef]
40. Yu, G.; Zhang, M.; Saha, M.L.; Mao, Z.; Chen, J.; Yao, Y.; Zhou, Z.; Liu, Y.; Gao, C.; Huang, F.; et al. Antitumor Activity of a Unique Polymer That Incorporates a Fluorescent Self-Assembled Metallacycle. *J. Am. Chem. Soc.* 2017, 139, 15940–15949. [CrossRef]

41. Zhou, J.; Zhang, Y.; Yu, G.; Crawley, M.R.; Fulong, C.R.P.; Friedman, A.E.; Sengupta, S.; Sun, J.; Li, Q.; Huang, F.; et al. Highly Emissive Self-Assembled BODIPY-Platinum Supramolecular Triangles. *J. Am. Chem. Soc.* 2018, 140, 7730–7736. [CrossRef] [PubMed]

42. Li, C.; Jia, P.-P.; Xu, Y.-L.; Ding, F.; Yang, W.-C.; Sun, Y.; Li, X.-P.; Yin, G.-Q.; Xu, L.; Yang, G.-F. Photoacoustic Imaging-Guided Chemo-Photothermal Combinational Therapy Based on Emissive Pt(II) Metallacycle-Loaded Biomimic Melanin Dots. *Sci. China Chem.* 2020. [CrossRef]

43. Zhu, H.; Shangguan, L.; Shi, B.; Yu, G.; Huang, F. Recent Progress in Macrocyclic Amphiphiles and Macrocyclic Host-Based Supra-Amphiphiles. *Mater. Chem. Front.* 2018, 2, 2152–2174. [CrossRef]

44. Chen, H.; Zhang, W.; Zhu, G.; Xie, J.; Chen, X. Rethinking Cancer Nanotheranostics. *Nat. Rev. Mater.* 2017, 2, 17024. [CrossRef] [PubMed]

45. Preston, D.; McNeill, S.M.; Lewis, J.E.M.; Giles, G.I.; Crowley, J.D. Enhanced Kinetic Stability of [Pd2L4]4+ Cages through Ligand Substitution. *Dalton Trans.* 2016, 45, 8050–8060. [CrossRef]

46. Petros, R.A.; DeSimone, J.M. Strategies in the Design of Nanoparticles for Therapeutic Applications. *Nat. Rev. Drug Discov.* 2010, 9, 615–627. [CrossRef]

47. Mansour, H.M.; Sohn, M.; Al-Ghananeem, A.; DeLuca, P.P. Materials for Pharmaceutical Dosage Forms: Molecular Pharmaceutics and Controlled Release Drug Delivery Aspects. *Int. J. Mol. Sci.* 2010, 11, 3298–3322. [CrossRef]

48. Wolfbeis, O.S. An Overview of Nanoparticles Commonly Used in Fluorescent Bioimaging. *Chem. Soc. Rev.* 2015, 44, 4743–4768. [CrossRef]

49. Akash, M.S.H.; Rehman, K. Recent Progress in Biomedical Applications of Pluronic (PF127): Pharmaceutical Perspectives. *J. Control. Release* 2015, 209, 123–138. [CrossRef]

50. Biswas, S.; Kumari, P.; Lakhan, P.M.; Ghosh, B. Recent Advances in Polymeric Micelles for Anti-Cancer Drug Delivery. *Eur. J. Pharm. Sci.* 2016, 83, 184–202. [CrossRef]

51. Jarak, I.; Varela, C.L.; Tavares da Silva, E.; Roleira, F.F.M.; Veiga, F.; Figueiras, A. Pluronic-Based Nanovehicles: Recent Advances in Anticancer Therapeutic Applications. *Eur. J. Med. Chem.* 2020, 206, 112526. [CrossRef] [PubMed]

52. Maeda, H. Tumor-Selective Delivery of Macromolecular Drugs via the EPR Effect: Background and Future Prospects. *Bioconjugate Chem.* 2010, 21, 797–802. [CrossRef]

53. Fang, J.; Nakamura, H.; Maeda, H. The EPR Effect: Unique Features of Tumor Blood Vessels for Drug Delivery, Factors Involved, and Limitations and Augmentation of the Effect. *Adv. Drug Deliv. Rev.* 2011, 63, 136–151. [CrossRef]

54. Yu, G.; Cook, T.R.; Li, Y.; Yan, X.; Wu, D.; Shao, L.; Shen, J.; Tang, G.; Huang, F.; Chen, X.; et al. Tetr phenylethene-Based Highly Emissive Metallacage as a Component of Theranostic Supramolecular Nanoparticles. *Proc. Natl. Acad. Sci. USA* 2016, 113, 13720–13725. [CrossRef]

55. Yue, Z.; Wang, H.; Bowers, D.J.; Gao, M.; Stilgenbauer, M.; Nielsen, F.; Shelley, J.T.; Zheng, Y.-R. Nanoparticles of Metal–Organic Cages Designed to Encapsulate Platinum-Based Anticancer Agents. *Dalton Trans.* 2018, 47, 670–674. [CrossRef] [PubMed]

56. Agostinis, P.; Berg, K.; Cengel, K.A.; Foster, T.H.; Giorotti, A.W.; Gollnick, S.O.; Hahn, S.M.; Hamblin, M.R.; Juzeniene, A.; Kessel, D.; et al. Photodynamic Therapy of Cancer: An Update. *CA Cancer J. Clin.* 2011, 61, 250–281. [CrossRef]

57. Dolmans, D.E.J.G.J.; Fukumura, D.; Jain, R.K. Photodynamic Therapy for Cancer. *Nat. Rev. Cancer* 2003, 3, 380–387. [CrossRef] [PubMed]

58. Master, A.; Livingstone, M.; Sen Gupta, A. Photodynamic Nanomedicine in the Treatment of Solid Tumors: Perspectives and Challenges. *J. Control. Release* 2013, 168, 88–102. [CrossRef]

59. Celli, J.P.; Spring, B.Q.; Rizvi, I.; Evans, C.L.; Samkoe, K.S.; Verma, S.; Pogue, B.W.; Hasan, T. Imaging and Photodynamic Therapy: Mechanisms, Monitoring, and Optimization. *Chem. Rev.* 2010, 110, 2795–2838. [CrossRef]

60. Yu, Y.; Xu, Q.; He, S.; Xiong, H.; Zhang, Q.; Xu, W.; Ricotta, V.; Bai, L.; Zhang, Q.; Yu, Z.; et al. Recent Advances in Delivery of Photosensitizing Metal-Based Drugs. *Coord. Chem. Rev.* 2019, 387, 154–179. [CrossRef]

61. Li, Y.; Lin, T.-y.; Luo, Y.; Liu, Q.; Xiao, W.; Guo, W.; Lac, D.; Zhang, H.; Feng, C.; Wachsmann-Hogiu, S.; et al. A Smart and Versatile Theranostic Nanomedicine Platform Based on Nanophosphor. *Nat. Commun.* 2014, 5, 4712. [CrossRef] [PubMed]

62. Lovell, J.E.; Liu, T.W.B.; Chen, J.; Zheng, G. Activatable Photosensitizers for Imaging and Therapy. *Chem. Rev.* 2010, 110, 2839–2857. [CrossRef] [PubMed]

63. Lovell, J.E.; Jin, C.S.; Huynh, E.; Jin, H.; Kim, C.; Rubinstein, J.L.; Chan, W.C.W.; Cao, W.; Wang, L.V.; Zheng, G. Porphyrine Nanovesicles Generated by Polypyrrole Bilayers as Use as Multimodal Biophotonic Contrast Agents. *Nat. Mater.* 2011, 10, 324–332. [CrossRef] [PubMed]

64. Gupta, G.; Denoyelle-Di-Muro, E.; Mbakidi, J.-P.; Leroy-Lhez, S.; Sol, V.; Therrien, B. Delivery of Porphin to Cancer Cells by Organometallic Rh(III) and Ir(III) Metalla-Cages. *J. Organomet. Chem.* 2015, 787, 44–50. [CrossRef]

65. Schmitt, F.; Freudenberg, J.; Barry, N.P.E.; Juillera-Jeanneret, L.; Süss-Fink, G.; Therrien, B. Organometallic Cages as Vehicles for Intracellular Release of Photosensitizers. *J. Am. Chem. Soc.* 2012, 134, 754–757. [CrossRef]

66. Jiang, X.; Zhou, Z.; Yang, H.; Shan, C.; Yu, H.; Wojtas, L.; Zhang, M.; Mao, Z.; Wang, M.; Stang, P.J. Self-Assembly of Porphyrin-Containing Metalla-Assemblies and Cancer Photodynamic Therapy. *Inorg. Chem.* 2020, 59, 7380–7388. [CrossRef]

67. Qin, Y.; Chen, L.-J.; Dong, F.; Jiang, S.-T.; Yin, G.-Q.; Li, X.; Tian, Y.; Yang, H.-B. Light-Controlled Generation of Singlet Oxygen within a Discrete Dual-Stage Metallacycle for Cancer Therapy. *J. Am. Chem. Soc.* 2019, 141, 8943–8950. [CrossRef]
68. Yu, G.; Yu, S.; Saha, M.L.; Zhou, J.; Cook, T.R.; Yung, B.C.; Chen, J.; Mao, Z.; Zhang, F.; Zhou, Z.; et al. A Discrete Organoplatinum(II) Metallacage as a Multimodality Theranostic Platform for Cancer Photochemotherapy. *Nat. Commun.* 2018, 9, 4335. [CrossRef] [PubMed]

69. Yu, G.; Zhu, B.; Shao, L.; Zhou, J.; Saha, M.L.; Shi, B.; Zhang, Z.; Hong, T.; Li, S.; Chen, X.; et al. Host–Guest Complexation-Mediated Codelivery of Anticancer Drug and Photosensitizer for Cancer Photochemotherapy. *Proc. Natl. Acad. Sci. USA* 2019, 116, 6618–6623. [CrossRef] [PubMed]

70. Zhang, D.-Y.; Zheng, Y.; Tan, C.-P.; Sun, J.-H.; Zhang, W.; Ji, L.-N.; Mao, Z.-W. Graphene Oxide Decorated with Ru(II)-Polyethylene Glycol Complex for Lysosome-Targeted Imaging and Photodynamic/Photothermal Therapy. *ACS Appl. Mater. Interfaces* 2017, 9, 6761–6771. [CrossRef] [PubMed]

71. Huang, H.; Yu, B.; Zhang, P.; Huang, J.; Chen, Y.; Gassner, G.; Ji, L.; Chao, H. Highly Charged Ruthenium(II) Polypryridyl Complexes as Lysosome-Localized Photosensitizers for Two-Photon Photodynamic Therapy. *Angew. Chem. Int. Ed.* 2015, 54, 14049–14052.

72. Liu, J.; Chen, Y.; Li, G.; Zhang, P.; Jin, C.; Zeng, L.; Ji, L.; Chao, H. Ruthenium(II) Polypryridyl Complexes as Mitochondria-Targeted Two-Photon Photodynamic Anticancer Agents. *Biomaterials* 2015, 56, 140–153. [PubMed]

73. Zhou, Z.; Liu, J.; Huang, J.; Rees, T.W.; Wang, Y.; Wang, H.; Li, X.; Chao, H.; Stang, P.J. A Self-Assembled Ru–Pt Metallacage as a Lysosome-Targeting Photosensitizer for 2-Photon Photodynamic therapy. *Proc. Natl. Acad. Sci. USA* 2019, 116, 20296–20302. [PubMed]

74. Ding, F.; Zhan, Y.; Lu, X.; Sun, Y. Recent Advances in Near-Infrared II Fluorophores for Multifunctional Biomedical Imaging. *Chem. Sci.* 2018, 9, 4370–4380.

75. Hong, G.; Antaris, A.L.; Dai, H. Near-Infrared Fluorophores for Biomedical Imaging. *Nat. Biomed. Eng.* 2017, 1, 1–22.

76. Miao, Q.; Pu, K. Organic Semiconducting Agents for Deep-Tissue Molecular Imaging: Second Near-Infrared Fluorescence, Self-Luminescence, and Photoacoustics. *Adv. Mater.* 2018, 30, 1801778.

77. Lu, L.; Li, B.; Ding, S.; Fan, Y.; Wang, S.; Sun, C.; Zhao, M.; Zhao, C.-X.; Zhang, F. NIR-II Bioluminescence for In Vivo High Contrast Imaging and In Situ ATP-Mediated Metastases Tracing. *Nat. Commun.* 2020, 11, 4192.

78. Wang, P.; Fan, Y.; Lu, L.; Liu, L.; Fan, L.; Zhao, M.; Xie, Y.; Xu, C.; Zhang, F. NIR-II Nanoprobes In-Vivo Assembly to Improve Image-Guided Surgery for Metastatic Ovarian Cancer. *Nat. Commun.* 2018, 9, 2898.

79. Sun, Y.; Ding, F.; Zhou, Z.; Li, C.; Pu, M.; Xu, Y.; Zhan, Y.; Lu, X.; Li, H.; Yang, G.; et al. Rhomboïdal Pt(II) Metallacycle-Based NIR-II Theranostic Nanoprobe for Tumor Diagnosis and Image-Guided Therapy. *Proc. Natl. Acad. Sci. USA* 2019, 116, 1968–1973.

80. Ding, F.; Chen, Z.; Kim, W.Y.; Sharma, A.; Li, C.; Ouyang, Q.; Zhu, H.; Yang, G.; Sun, Y.; Kim, J.S. A Nano-Cocktail of an NIR-II Emissive Fluorophore and Organoplatinum(II) Metallacycle for Efficient Cancer Imaging and Therapy. *Chem. Sci.* 2019, 10, 7023–7028.

81. Fan, Q.; Cheng, K.; Hu, X.; Ma, X.; Zhang, R.; Yang, M.; Lu, X.; Xing, L.; Huang, W.; Gambhir, S.S.; et al. Transferring Biomarker into Molecular Probe: Melanin Nanoparticle as a Naturally Active Platform for Multimodality Imaging. *J. Am. Chem. Soc.* 2014, 136, 15185–15194. [CrossRef] [PubMed]

82. Fan, B.; Yang, X.; Li, X.; Lv, S.; Zhang, H.; Sun, J.; Li, L.; Wang, L.; Qu, B.; Peng, X.; et al. Photoacoustic-Imaging-Guided Therapy of Functionalized Melanin Nanoparticles: Combination of Photothermal Ablation and Gene Therapy against Laryngeal Squamous Cell Carcinoma. *Nanoscale* 2019, 11, 6285–6296. [CrossRef] [PubMed]

83. Zhang, R.; Fan, Q.; Yang, M.; Cheng, K.; Lu, X.; Zhan, L.; Huang, W.; Cheng, Z. Engineering Melanin Nanoparticles as an Efficient Drug-Delivery System for Imaging-Guided Chemotherapy. *Adv. Mater.* 2015, 27, 5063–5069. [CrossRef] [PubMed]

84. Solano, F. Melanins: Skin Pigments and Much More—Types, Structural Models, Biological Functions, and Formation Routes. *New J. Sci.* 2014, 2014, 498276. [CrossRef]

85. Sun, Y.; Ding, F.; Chen, Z.; Zhang, R.; Li, C.; Xu, Y.; Zhang, Y.; Ni, R.; Li, X.; Yang, G.; et al. Melanin-Dot-Mediated Delivery of Metallacycle for NIR-II/Photoacoustic Dual-Modal Imaging-Guided Chemo-Photothermal Synergistic Therapy. *Proc. Natl. Acad. Sci. USA* 2019, 116, 16729–16735. [CrossRef] [PubMed]

86. Lim, E.-K.; Kim, T.; Paik, S.; Haam, S.; Huh, Y.-M.; Lee, K. Nanomaterials for Theranostics: Recent Advances and Future Challenges. *Chem. Rev.* 2015, 115, 327–394. [CrossRef] [PubMed]

87. Yao, Y.; Zhao, R.; Shi, Y.; Cai, Y.; Chen, J.; Sun, S.; Zhang, W.; Tang, R. 2D Amphiphilic Organoplatinum(II) Metallacycles: Their Syntheses, Self-Assembly in Water and Potential Application in Photodynamic therapy. *Chem. Commun.* 2018, 54, 8068–8071. [CrossRef] [PubMed]

88. Li, Y.; Yuan, X.; Yu, J.; Fan, Y.; He, T.; Lu, S.; Li, X.; Qiu, H.; Yin, S. Amphiphilic Rhomboïdal Organoplatinum(II) Metallacycles with Encapsulated Doxorubicin for Synergistic Cancer Therapy. *ACS Appl. Bio Mater.* 2020, 3, 8061–8068. [CrossRef]

89. Zhao, D.; Tan, S.; Yuan, D.; Lu, W.; Rezenom, Y.H.; Jiang, H.; Wang, L-Q.; Zhou, H-C. Surface Functionalization of Porous Coordination Nanocages Via Click Chemistry and Their Application in Drug Delivery. *Adv. Mater.* 2011, 23, 90–93. [CrossRef] [PubMed]

90. Murray, J.; Kim, K.; Ogoshi, T.; Yao, W.; Gibb, B.C. The Aqueous Supramolecular Chemistry of Cucurbit[n]urils, Pillar[n]arenes and Deep-Cavity Cavitands. *Chem. Soc. Rev.* 2017, 46, 2479–2496. [CrossRef]

91. Lee, J.W.; Samal, S.; Selvapalan, N.; Kim, H.-J.; Kim, K. Cucurbituril Homologues and Derivatives: New Opportunities in Supramolecular Chemistry. *Accounts Chem. Res.* 2003, 36, 621–630. [CrossRef] [PubMed]

92. Kim, J.; Jung, I.-S.; Kim, S.-Y.; Lee, E.; Kang, J.-K.; Sakamoto, S.; Yamaguchi, K.; Kim, K. New Cucurbituril Homologues: Syntheses, Isolation, Characterization, and X-ray Crystal Structures of Cucurbit[n]uril (n = 5, 7, and 8). *J. Am. Chem. Soc.* 2000, 122, 540–541. [CrossRef]
93. Nagahama, K.; Utsumi, T.; Kumano, T.; Maekawa, S.; Oyama, N.; Kawakami, J. Discovery of a New Function of Curcumin Which Enhances Its Anticancer Therapeutic Potency. Sci. Rep. 2016, 6, 30962. [CrossRef] [PubMed]

94. Datta, S.; Misra, S.K.; Saha, M.L.; Lahiri, N.; Louie, J.; Pan, D.; Stang, P.J. Orthogonal Self-Assembly of an Organoplatinum(II) Metallacycle and Cucurbit[8]uril That Delivers Curcumin to Cancer Cells. Proc. Natl. Acad. Sci. USA 2018, 115, 8087–8092. [CrossRef]

95. Lee, C.C.; MacKay, J.A.; Fréchet, J.M.J.; Szoka, F.C. Designing Dendrimers for Biological Applications. Nat. Biotechnol. 2005, 23, 1517–1526. [CrossRef]

96. Svenson, S.; Tomalia, D.A. Dendrimers in Biomedical Applications—Reflections on the Field. Adv. Drug Deliv. Rev. 2005, 57, 2106–2129. [CrossRef]

97. Astruc, D.; Boisselier, E.; Ornelas, C. Dendrimers Designed for Functions: From Physical, Photophysical, and Supramolecular Properties to Applications in Sensing, Catalysis, Molecular Electronics, Photonics, and Nanomedicine. Chem. Rev. 2010, 110, 1857–1959. [CrossRef]

98. Astruc, D.; Ornelas, C.; Ruiz, J. Metallocenyl Dendrimers and Their Applications in Molecular Electronics, Sensing, and Catalysis. Accounts Chem. Res. 2008, 41, 841–856. [CrossRef]

99. Chen, L.J.; Zhao, G.-Z.; Jiang, B.; Sun, B.; Wang, M.; Xu, L.; He, J.; Abliz, Z.; Tan, H.; Li, X.; et al. Smart Stimuli-Responsive Spherical Nanostructures Constructed from Supramolecular Metallodendrimers via Hierarchical Self-Assembly. J. Am. Chem. Soc. 2014, 136, 5993–6001. [CrossRef]

100. Wang, C.; Wang, Z.; Zhang, X. Amphiphilic Building Blocks for Self-Assembly: From Amphiphiles to Supra-Amphiphiles. Accounts Chem. Res. 2012, 45, 608–618. [CrossRef]

101. Chang, Y.; Jiao, Y.; Symons, H.E.; Xu, J.-F.; Faul, C.F.J.; Zhang, X. Molecular Engineering of Polymeric Supra-Amphiphiles. Chem. Soc. Rev. 2019, 48, 989–1003. [CrossRef] [PubMed]

102. Samanta, S.K.; Moncelet, D.; Briken, V.; Isaacs, L. Metal–Organic Polyhedron Capped with Cucurbit[8]uril Delivers Doxorubicin to Cancer Cells. J. Am. Chem. Soc. 2016, 138, 14488–14496. [CrossRef] [PubMed]

103. Samanta, S.K.; Quigley, J.; Vinciguerra, B.; Briken, V.; Isaacs, L. Cucurbit[7]uril Enables Multi-Stimuli-Responsive Release from the Self-Assembled Hydrophobic Phase of a Metal Organic Polyhedron. J. Am. Chem. Soc. 2017, 139, 9066–9074. [CrossRef] [PubMed]

104. Hu, X.; Zhang, Y.; Xie, Z.; Jing, X.; Bellotti, A.; Gu, Z. Stimuli-Responsive Polymersomes for Biomedical Applications. Biomacromolecules 2017, 18, 649–673. [CrossRef]

105. Zhang, Q.; Re Ko, N.; Kwon Oh, J. Recent advances in stimuli-responsive degradable block copolymer micelles: Synthesis and controlled drug delivery applications. Chem. Commun. 2012, 48, 7542–7552. [CrossRef]

106. Zhou, J.; Yu, G.; Yang, J.; Shi, B.; Ye, B.; Wang, M.; Huang, F.; Stang, P.J. Polymeric Nanoparticles Integrated from Discrete Organoplatinum(II) Metallacycle by Stepwise Post-assembly Polymerization for Synergistic Cancer Therapy. Chem. Mater. 2020, 32, 4564–4573. [CrossRef]