Modeling COVID-19 dynamics in Illinois under non-pharmaceutical interventions

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We present modeling of the COVID-19 epidemic in Illinois, USA, capturing the implementation of
a Stay-at-Home order and scenarios for its eventual release. We use a non-Markovian age-of-infection
model that is capable of handling long and variable time delays without changing its model topology.
Bayesian estimation of model parameters is carried out using Markov Chain Monte Carlo (MCMC)
methods. This framework allows us to treat all available input information, including both the
previously published parameters of the epidemic and available local data, in a uniform manner. To
accurately model deaths as well as demand on the healthcare system, we calibrate our predictions to
total and in-hospital deaths as well as hospital and ICU bed occupancy by COVID-19 patients. We
apply this model not only to the state as a whole but also its sub-regions in order to account for the
wide disparities in population size and density. Without prior information on non-pharmaceutical
interventions (NPIs), the model independently reproduces a mitigation trend closely matching
mobility data reported by Google and Unacast. Forward predictions of the model provide robust
estimates of the peak position and severity and also enable forecasting the regional-dependent results
of releasing Stay-at-Home orders. The resulting highly constrained narrative of the epidemic is able
to provide estimates of its unseen progression and inform scenarios for sustainable monitoring and
control of the epidemic.

On January 24, 2020, the second known COVID-19
case to be diagnosed in the USA was reported in Chicago,
Illinois. Community transmission of the disease was con-
firmed on March 8, 2020. During the subsequent ten days,
the epidemic grew with a case doubling time of approxi-
ately 2.3 days, while testing capacity was essentially
fixed. On March 21, 2020, a Stay-at-Home order was
issued for the entire state of Illinois and subsequently
extended on March 31, 2020 and again on April 23, 2020.
The order was lifted on May 30, 2020 [1]. Responsible re-
 laxation of the mitigation of COVID-19 must be informed
by realistic and well-calibrated epidemiological modeling
of the outcomes of any scenarios under consideration—not
just of the resulting (increased) death toll but also of the
stress placed upon the healthcare system. The purpose
of this report is to present such an analysis.

A variety of modeling approaches are used by hospi-
tals, public health officials, and state governments. These
range between phenomenological models that use a curve-
fitting procedure to match data, such as the daily death
rate, and mechanistic methods that model the trajectory
of the epidemic as individuals transition through several
disease and healthcare-bound stages [2–5]. Only mechan-
astic models are able to make justifiable predictions
while accounting for changes in the epidemic environ-
ment, such as the imposition or relaxation of community
mitigation efforts. Of these, compartmental models like
the Susceptible-Infectious-Recovered (SIR) models, and
Susceptible-Exposed-Infectious-Recovered (SEIR) exten-
sions, are widely used. Compartmental models describe
how fractions of a homogeneous, well-mixed population
progress through different states the disease, driven by
interactions between infectious and susceptible individu-
als. In the simplest models, the dynamics is deterministic
and the rates are constant in time, but many variants and
extensions exist and are widely used.

In order to be practically useful, models must be cal-
ibrated to observed data [3, 4, 8]. We calibrate the im-
portant dynamics of the model to several simultaneous
streams of empirical data including total and in-hospital
deaths, as well as hospital and ICU bed occupancy by
COVID-19 patients. To avoid biases resulting from non-
uniform and non-constant testing rates, which may be
difficult to parameterize, we do not consider positive case
data. The resulting model is a description of the epidemic
as it progresses through the hospital system in Illinois;
as it is clear that a non-negligible number of COVID-19
deaths occur outside the hospital environment (e.g., in
homes and nursing homes especially), we augment our
model with an effective description of the net incidence
of deaths due to COVID-19.

There are many limitations to the types of models
that we and others use to describe COVID-19, and these
have been explored extensively in the literature, especially
with regards to spatial structure [9], superspreader events
and individuals [10, 13], and the structure of contact net-
works [14–16]. A geographical region as large as the state
of Illinois is not well-described as homogeneous, due to
large variations in population density and prevalence of infection between the Chicago metropolitan area and the more rural regions in Central and Southern Illinois. Indeed, most of the known cases and deaths to date have occurred in the Chicago area (by roughly an order of magnitude), so in practice this region dominates our results for the state as a whole.

One cannot simply scale the results of models for the Chicago metropolitan area to the entire state, however, because the transmission characteristics depend on the frequency and duration of contacts, which likely vary significantly among geographical regions. For this reason, we simulate the dense urban areas and the three sparser, more rural areas separately. We note that a more refined treatment would account for transfers between these separate populations, as well as transfers into and out of the state as a whole; however, we do not currently model these processes. The number of cases in individual rural areas is sufficiently small, due to the early Stay-At-Home order, that a long phase of exponential growth in these regions was largely avoided. As a result, these populations are not well-described by continuum, deterministic models. Nevertheless, by aggregating these populations, the numbers are large enough that deterministic, exponential growth, at least at the early stages, was visible.

In this work, we describe an estimate of the rise and fall of the epidemic within Illinois, taking into account the modulation of the transmission parameters due to social distancing. In the following sections, we first describe our extension of the SEIR model, which takes into account the long and variable delay times reported in the literature. After describing the procedure by which we calibrate the model to data, we argue for the robustness of short term model predictions. Finally, we present and discuss our predictions of the epidemic trajectory through the Summer of 2020, including the effects of the release of the Stay-at-Home order at the end of May.

I. MODEL DESCRIPTION

To facilitate a general treatment of delay times in the COVID-19 epidemic, we implement a non-Markovian model that derives from the classic Kermack-McKendrick age-of-infection model [17]. Age-of-infection models are similar to compartmental models, such as Susceptible-Infectious-Recovered (SIR) or Susceptible-Exposed-Infectious-Recovered (SEIR) models, but allow transition delays between entering sequential states to be drawn from arbitrary probability density functions (see, e.g. [4, 18]). We use non-Markovian models because their delays can be defined by an arbitrary number of timescales, in contrast to the single exponential rate parameter of compartment based models. Non-Markovian models are thus, in principle, better able to reproduce the observed signal delays between different states, e.g., the flattening of the curve of hospital admissions compared to in-hospital deaths.

The use of deterministic rather than stochastic epidemic descriptions is generally justified when the modeled populations are large enough that relative daily changes are small and the number of individuals is large relative to one. This means that a deterministic compartmental model has a self-consistency check, because once the epidemic size is of order unity, a stochastic model allows the epidemic to die out; in contrast, in a deterministic model an epidemic will continue to evolve even with an unrealistic, fractional number of infectious individuals. We will see that for some regions of Illinois, our estimates are at the limit of validity of deterministic models.

We adapt the conventional age-of-infection model to include a number of delayed healthcare system observables of the epidemic, such as the number of patients in hospitals, Intensive Care Units (ICUs), and ultimately, the number of deaths.

A. Time-modulated age-of-infection model

The core of our model is the daily incidence (i.e., the number of newly-infected individuals) in demographic (age) group $i$, $j_i(t)$. This value determines the dynamics of susceptible individuals in that group $S_i(t)$ according to

$$\frac{dS_i(t)}{dt} = -j_i(t).$$

(1)

The incidence itself follows the renewal equation,

$$j_i(t) = R_t \frac{S_i(t)}{S(t)} \sum_m \xi_{im} \int_0^\infty d\tau K_{\text{serial}}(\tau) j_m(t - \tau).$$

(2)

Here, $R_t$ is time-dependent effective reproduction number, $S(t) = \sum_i S_i(t)$ is the total susceptible population, $K_{\text{serial}}(\tau)$ is the probability density function (PDF) of serial intervals, and $\xi_{im}$ is the contact matrix. For simplicity, we assume $\xi_{im} = 1$, i.e., all demographic groups infect each other at the same rate. We assume that $N_i$, the total number of individuals in the demographic group $i$, is approximately constant for the duration of the epidemic. In practice, this means our model neglects the effects of births, deaths due to causes unrelated to COVID-19, and mobility of the population, which is appropriate for the short time scales we model. We further assume that individuals are only infected once, i.e., that the duration of immunity to COVID-19 is longer than the timescale over which we simulate the epidemic. Our simulations begin on a day $t_s$ (whose value we sample during parameter inference) at which point we impose that ten people are spontaneously infected, setting $j_i(t)$ in proportion to the age distribution of the population under study.

We parameterize the effective reproduction number $R_t$ in terms of the basic reproduction number $R_0$, a seasonal forcing factor $F(t)$, a mitigation factor $M(t)$, and the susceptible population fraction $S(t)/N$ according to

$$R_t = R_0 F(t) M(t) \frac{S(t)}{N}. \quad (3)$$
The formal dependence of $R_0$ on the total susceptible population $S(t)$ is corrected in Eq. 2 by a factor $S(t)/S(t)$ which accounts for possible variation of susceptibility between different demographic groups. In our model, the homogeneous factor $M(t)$ accounts for all sources of mitigation, including the effects of self-imposed isolation as well as government-mandated Stay-at-Home (SAH) orders, school closures, etc. We parameterize $M(t)$ as a piecewise cubic Hermite interpolating polynomial that smoothly interpolates from 1 at $t_0$ to $M(t_1)$ at $t_1$, and is otherwise constant. The mitigation factor $M(t_1)$, start time, and end time of the interpolation interval are fitted by our algorithm. We choose to parameterize $M(t)$ as a single transition (i.e., a single event) since this minimal model reduces the risk of overfitting to spurious trends. This choice is supported by the following observations: the adoption of social distancing practices took place relatively rapidly over a one to two week period; and the Stay-at-Home order remained active after the initial transition, presumably suppressing the magnitude of changes to mitigation. We will observe that this choice is a sufficient approximation for the duration of the data we use for calibration. We evaluate these claims more explicitly Section III D.

To model seasonal effects, we follow Ref. 19, which estimates seasonal forcing from the observed seasonal variability of positive tests in three other endemic coronaviruses. We thus adopt the functional form

$$F(t) = 1 + A_{SF} \cos \left( \frac{2\pi (t - t_{peak})}{365} \right),$$

(4)

where $A_{SF}$ denotes the strength of the forcing and $t_{peak}$ sets the day of the year when seasonal forcing is strongest. From Ref. 19, we infer that seasonal forcing is strongest in the winter and set $t_{peak} = January 16$.

Ref. 19 finds evidence for $A_{SF} \approx 0.2$; however, we account for uncertainty in this parameter by sampling over $A_{SF}$ during parameter inference. Incorporating this uncertainty is critical: if mitigation were only able to reduce the effective reproduction number to roughly unity, then seasonal forcing could drive a second wave of the epidemic.

For timescales of only a few months, our parameterization of $R_0$ includes a degeneracy: a change in the parameter $A_{SF}$ may be compensated by adjusting the mitigation profile $M(t)$. The degeneracy is broken as data is collected over long timescales, since $M(t)$ models relatively instantaneous changes in infectiousness and $F(t)$ produces an explicitly year-long, periodic modulation. Practically, this implies that $A_{SF}$ may account for both seasonal effects and concurrent slow variations in the mitigation factor.

B. Model topology

Due to limited and biased testing, neither the susceptible population $S_i(t)$ nor the daily incidence of new infection cases $j_i(t)$ are directly observable. Hence, we are forced to infer the dynamics of the epidemic using lagging and indirect indicators. These indicators include the total number of hospitalized (but not critical) patients $H(t)$, the number of critically ill patients currently in ICU beds $C(t)$, and $D(t)$, the cumulative number of daily deaths in the hospital.

Our model topology assumes that all hospital deaths occur in ICU rooms. In practice, this simplification would be invalid if either a significant number of individuals die immediately upon entering the hospital (i.e., if the true delay distribution between hospitalization and death is appreciably bimodal), or if the number of hospital deceidents exceeds the number of individuals who are admitted to the ICU. In this sense, our inferred parameter values, e.g., the probability of a patient in critical care dying, should not be interpreted as having real-world meaning, since the values accommodate approximations in order to fit all input data.

Furthermore, by separating the observables from the incidence dynamics, our model supposes that that the hospitalization status of an individual does not affect their likelihood of infecting someone. This choice is appropriate if the number of hospitalized individuals is a small fraction of the total number of infected individuals, or if the delay between infection and hospitalization is longer than the serial interval.

The dynamics of the system may be described by daily flux variables:

- $\sigma_i(t)$, the number of infected individuals who become symptomatic
- $h_i(t)$, the number of daily admissions to all hospitals
- $r_i(t)$, the daily number of patients discharged from all hospitals
- $c_i(t)$, the daily number of patients transferred from the main floor of a hospital to its ICU
- $v_i(t)$, the daily number of patients transferred from the ICU to the main floor of a hospital, and
- $d_i(t)$, the daily number of deaths in ICU rooms.

We do not directly model deaths that happen outside of hospitals but instead infer the ratio of these deaths to the hospital deaths during our fitting procedure, as described below. Figure 1 schematically depicts the topology of our model along with the names of all flux and cumulative variables.

The dynamics of any flux variable $y(t)$ defined above may be obtained from the variable $x(t)$ directly preceding it in the chain of events shown in Fig. 1:

$$y(t) = p_y \int_0^\infty d\tau K_y(\tau)x(t-\tau).$$

Here, $p_y$ is the proportion of individuals undergoing the transition $x \rightarrow y$ with time delays distributed according...
FIG. 1. The topology of our model along with the names of all flux and state variables: the daily incidence, $j(t)$; the daily number of newly symptomatic individuals, $\sigma(t)$; the number of daily admissions to all hospitals, $h(t)$; the daily number of patients discharged from all hospitals, $r(t)$; the daily number of patients transferred from the main floor of a hospital to its ICU, $c(t)$; the daily number of deaths in hospitals, $d(t)$; and the daily number of deaths in and out of hospitals, $d_{\text{tot}}(t)$. State variables are: the total number of occupied hospital beds (main floor) $H(t)$, and the total number of occupied ICU beds $C(t)$. The other parameters of the model are the fractions of infected individuals who ever become symptomatic, $p_{\sigma,i}$; the fraction of symptomatic individuals who are ever hospitalized, $p_{h,i}$; the fraction of hospital patients who ever get to ICU, $p_{c,i}$; and the fraction of ICU patients who will ultimately die $p_{d,i}$; and the multiplier, $F_{\text{tot}}$ that converts between hospital deaths and all deaths in the state, including those outside of the hospital system. For the sake of legibility, we suppress age-group indices in the diagram.

to a probability density function $K_\sigma(t)$. Note that Eq. 2 has the same structure except that both the input $x$ and the output $y$ variables are given by the daily incidence $j_i(t)$.

For the flux variables defined above, one obtains the following equations. The number of infected individuals who become symptomatic is

$$\sigma_i(t) = p_{\sigma,i} \int_0^\infty d\tau K_\sigma(\tau) j_i(t - \tau), \quad (6)$$

where $p_{\sigma,i}$ is the (age-dependent) fraction of infected individuals who ever develop symptoms and $K_\sigma(\tau)$ is the PDF of the incubation period. The fraction $p_{h,i}$ of symptomatic individuals who are ever admitted to the hospital is

$$h_i(t) = p_{h,i} \int_0^\infty d\tau K_h(\tau) \sigma_i(t - \tau). \quad (7)$$

The flux of hospital patients who become critically ill and are admitted to the ICU is given by

$$c_i(t) = p_{c,i} \int_0^\infty d\tau K_c(\tau) h_i(t - \tau), \quad (8)$$

of which a fraction $p_{d,i}$ ultimately die according to

$$d_i(t) = p_{d,i} \int_0^\infty d\tau K_d(\tau) c_i(t - \tau). \quad (9)$$

The fraction $1 - p_{d,i}$ of ICU patients who stabilize and return to the general ward of the hospital do so according to

$$v_i(t) = (1 - p_{d,i}) \int_0^\infty d\tau K_v(\tau) c_i(t - \tau). \quad (10)$$

Both stabilized patients and hospital patients who recover without requiring critical care are discharged, thus the influx of recovered individuals due to hospital discharges is given by

$$r_i(t) = \int_0^\infty d\tau K_r(\tau) \left[ (1 - p_{c,i}) h_i(t - \tau) + v_i(t - \tau) \right]. \quad (11)$$

Finally, to approximately account for patients who die outside of the hospital system, we introduce $d_{\text{tot}}$, a variable that tracks the total number of daily deaths both within and outside of the hospital. We connect total deaths to hospital deaths $d$ according to a prefactor $F_{\text{tot}} \geq 1$ and delay time $\tau_{\text{tot}}$ that reflects bureaucratic delays associated with issuing deaths certificate and publishing data on the Illinois Department of Public Health (IDPH) website. We observe that these bureaucratic delays manifest themselves in strong day-of-the-week effects.

$$d_{\text{tot},i}(t) = F_{\text{tot}} \int_0^\infty d\tau K_{\text{tot}}(\tau) d_i(t - \tau). \quad (12)$$

In our simulations, we draw on clinical data to specify the age-dependent rates for hospitalization, ICU admission, and death. We report the details of this severity model in Table S1. To account for differences between the literature values and what has occurred in Illinois, we introduce age-independent prefactors for the transition rates and fit them in our simulations. Although the relative severity values we use may not be accurate, in practice this choice does not affect our model dynamics. Because the contact matrix $\xi_{\text{int}}$ is constant across all interactions, and because the susceptibility is not a function of demographic group, the demographic-aggregated statistics are insensitive to the relative demographic ratios. Then, since we only fit data that has been summed over
all age groups, we cannot observe any differences caused by inaccurate severity ratios.

The instantaneous occupation of hospital beds \( H(t) \) and of ICU beds \( C(t) \) may be obtained by integrating the incoming and outgoing fluxes as

\[
H(t) = \sum_{i} \int_{0}^{t} dt' [h_i(t') - c_i(t') + v_i(t') - r_i(t')]
\]

(13)

\[
C(t) = \sum_{i} \int_{0}^{t} dt' [c_i(t') - v_i(t') - d_i(t')],
\]

(14)

while the cumulative numbers of hospital and total deaths are

\[
D(t) = \sum_{i} \int_{0}^{t} dt' d_i(t')
\]

(15)

\[
D_{\text{tot}}(t) = \sum_{i} \int_{0}^{t} dt' d_{\text{tot},i}(t')
\]

(16)

II. PARAMETER INFERENCE

We calibrate our model to data by sampling over the high-dimensional model parameter space using a Markov chain Monte Carlo (MCMC) approach, as has been done by many others for epidemics in general (see, e.g. [7, 20]) and also for COVID-19 (see, e.g. for applications in China [21], Mexico [22] and Italy [23]). While standard optimization techniques can also identify the best-fit model parameters, we use MCMC because it produces an estimate of the global posterior probability distribution. With the full distribution, we can motivate bounds on parameter uncertainty, explore correlations between parameters, and identify model idiosyncrasies. Access to the full distribution also provides a direct means to marginalize over some modeling uncertainties when forecasting the future trajectory of the epidemic.

A. Markov chain Monte Carlo methods

Given a set of model parameters \( \vec{\Theta} \) and data \( \vec{D} \), the input to the MCMC sampler comprises a prior \( \pi(\vec{\Theta}) \) and a likelihood function \( L(\vec{D}|\vec{\Theta}) \). The sampler computes the posterior probability \( p(\vec{\Theta}|\vec{D}) \) for each point in parameter space according to Bayes’s theorem

\[
p(\vec{\Theta}|\vec{D}) = \frac{L(\vec{D}|\vec{\Theta})\pi(\vec{\Theta})}{Z(\vec{D})}
\]

(17)

The likelihood \( L \) represents the probability of observing the data \( \vec{D} \) given a model with input parameters \( \vec{\Theta} \), and the prior \( \pi \) encodes our expectation for the probability of a given set of model parameters \( \vec{\Theta} \). Because we only compare points within the posterior distribution for an individual set of data, we neglect the constant model evidence by setting \( Z(\vec{D}) = 1 \). In practice, the MCMC sampling recovers the log of the posterior probability distribution

\[
H(\vec{\Theta}|\vec{D}) = \ln \left[ L(\vec{D}|\vec{\Theta}) \right] - \frac{1}{2} \sum_{\alpha} \frac{(\Theta_{\alpha} - \Theta_{\alpha}^{(0)})^2}{\Delta_{\alpha}^2}
\]

(18)

Here, the second term is the log of the prior over the model parameters; for each parameter we either implement a Gaussian prior with mean expected value \( \Theta_{\alpha}^{(0)} \) and variance \( \Delta_{\alpha}^2 \), or we use a flat prior in which case the parameter does not appear in the sum.

This Bayesian framework enables a universal treatment of all available input information information, i.e., both observed time series data and the parameters of the model. We determine the prior means by averaging published clinical data weighted in proportion to the sample size of each study. To account for differences between reported estimates of parameters due to, e.g., possible variability of model parameters between different locations, the tolerance parameters \( \Delta_{\alpha} \) were estimated as unweighted root-mean-square deviations of the published data from their respective average values \( \Theta_{\alpha}^{(0)} \) across the different studies. As a result, our procedure is flexible with respect to any local variability in model parameters. If high quality local data on parameter values are available for calibration, as might be the case for the duration of ICU stays or severity models, these data can be used directly with small values (or zero) for the respective tolerance parameters. By forcing parameters with known values to be more tightly constrained, unknown parameters will be automatically optimized with respect to all data types, and we can thus increase the fidelity of our model calibration result.

Many of our model outputs and data quantify daily incidences, e.g., the number of deaths per day. For these sorts of rate data, a Poisson likelihood estimator is appropriate. For a data point \( d \) at time \( t \), the Poisson likelihood is given by

\[
L(\lambda|t, d) = \left( \frac{e^{-\lambda(t)} \lambda(t)^d}{d!} \right)^{1/T}
\]

(19)

where the time-dependent rate \( \lambda(t) \) is equal to the model output and \( T \) is the correlation time for the data. The likelihood over the full data set is the product over the likelihoods for each individual data point; thus, the total log-likelihood is given by

\[
\ln \left[ L(\vec{D}|\vec{\Theta}) \right] = \sum_{i} \ln \frac{\lambda(t_i) - \lambda(t_i) - \ln(\lambda(t_i))}{T_i}
\]

(20)

In addition to being a well-motivated choice when comparing count data to rates, the Poisson likelihood is appealing because its effective uncertainty scales with the
rate parameter. Thus, unlike with the $L_2$ norm, a single parameter specifies both the expectation value and the uncertainty of the measurement. In practice, we found that evaluating likelihoods using the $L_2$ norm did not significantly alter the qualitative features of our forecasts.

We divide by $T$ in Eq. 20 because we also calibrate against instantaneous hospital statistics, such as occupancy in the general ward and in the ICU. These data sources have natural correlation timescales: occupancies correspond to smoothed averages since the majority of individuals who occupy a bed do so continuously over several days. We set $T$ equal to the correlation timescales $\Theta^{(0)}$ from our priors. In particular, we assume a correlation of 6 days for occupied hospital beds, and a correlation of 12.75 days for occupied ICU beds. We set $T = 1$ for the raw incidence data, i.e., for daily hospital deaths and for daily total deaths.

In Table I we enumerate the model parameters we sample over and list the bounds on those parameters’ values. We also describe the shape of any prior distributions we impose. In our model, we use gamma distributions to describe delays, and specify the mean and standard deviation for each distribution. Here, the mean $\tau$ and standard deviation $\sigma$ of a gamma distribution are related to the standard shape and scale parameters by $k = \tau^2/\sigma^2$ and $\theta = \sigma^2/\tau$, respectively. We fix the serial interval mean and standard deviation to 4 and 3 days respectively [24, 25], while our incubation time distribution has fixed mean 5.5 days and a standard deviation of 2 days [26, 27]. Parameters for all other delays are sampled.

Finally, we implement MCMC sampling using the Python package emcee [33]. To improve sampling efficiency, we use ensemble move proposals based on the differential evolution [34], differential evolution snoozer [35], and kernel density [36] proposal updates.

### B. Posterior distributions and data fitting

We calibrate our model using data on hospital and ICU room occupancy by COVID-19 patients, the number of daily deaths of COVID-19 confirmed patients in hospitals, and the total number of daily deaths as publicly reported by the IDPH [37]. At the time of calibration, the hospitalization and ICU data were not publicly available and were provided to us by the IDPH. The MCMC sampling procedure produces a high-dimensional posterior probability. We use this posterior to identify the expectation values and uncertainties for each parameter with respect to the model and the data.

To summarize the posterior distribution in terms of epidemic trajectories, we take a representative sample of parameters $\Theta_\ast$ according to their posterior probabilities. For each $\Theta_\ast$, we simulate the full course of the epidemic, and we plot the resulting family of curves in aggregate. At every time point we identify the median values of all measurable quantities (hospital and ICU rooms, and deaths) as well as quantiles corresponding to 68.4% and 95.6% confidence intervals. Because these quantiles are evaluated independently at each point in time, the visually recognizable curves do not correspond to actual epidemic trajectories.

### III. MODELING RESULTS

We used our age-of-infection model to describe the progression of COVID-19 in Illinois during 2020. We performed analyses for the state and for four distinct localities of the state. We also considered three separate scenarios of social distancing in our modeling.

### A. Simulations for Illinois

In Fig. 2 we show the fits and predictions of our model for the entire state of Illinois assuming that once im-

| Parameter | Bounds | $\Theta^{(0)}$ | $\Delta$ |
|-----------|--------|----------------|---------|
| $R_0$     | [1, 5] |                |         |
| $\tau_s$  | [35, 65]|                |         |
| $t_0$     | [60, 85]|                |         |
| $t_1$     | [70, 100]|              |         |
| $M(t_1)$  | 0.05, 1|                |         |
| IFR       | 0.25%, 1.8% | 0.7% | 0.175* |
| $\tau_h$  | 0.5, 40| 6.5 | 2 |
| $\sigma_h$| 0.5, 20| 4  | 2 |
| $\tau_{disch}$ | 0.5, 40| 6  | 2 |
| $\sigma_{disch}$ | 0.5, 20| 4  | 2 |
| $p_c$     | 0.05, 4|                |         |
| $\tau_c$  | 0.5, 10| 2  | 2 |
| $\sigma_c$| 0.5, 10| 2  | 2 |
| $p_d$     | 0.05, 3|                |         |
| $\tau_d$  | 4, 20 | 12 | 3 |
| $\sigma_d$| 1, 20 | 8.5 | 3 |
| $\tau_{rec}$ | 4, 20 | 12.75 | 3 |
| $\sigma_{rec}$ | 1, 20 | 10 | 3 |
| $F_{tot}$ | 1, 10 |                |         |
| $\sigma_{tot}$ | 0, 10 | 2  | 1 |
| $\sigma_{tot}$ | 0, 10 | 2  | 1 |
| $A_{IFR}$ | 0, 0.2|                |         |

*We implement a Gaussian prior for $\ln IFR$, with mean corresponding to $IFR = 0.7\%$ and variance of $\ln IFR$ set to 0.175.
plemented, the state-imposed and self-regulated social distancing behavior of the population maintains the same level until the end of the simulation. We report the median and the 68.4% and 95.6% confidence intervals of several dynamical outputs of our model, obtained from an ensemble of forward simulations that sample the posterior distribution over model parameters. Fig. 2 presents three separate calibrations: (a) using data up through April 20, 2020 and assuming a fixed seasonal forcing amplitude $A_{SF} = 0.2$, (b) again using data through April 20, 2020 but instead sampling over $A_{SF}$, and (c) using data through May 17, 2020 and sampling over $A_{SF}$.

First, comparing panels (a) and (b) demonstrates that a 20% seasonal forcing effect produces a worse projection and may be an overestimate; while our model does not infer the origin of any yearly, periodic modulation to $R_t$ (or lack thereof), by mid May the forecasts disagree with the data. By contrast, the uncertainty introduced by sampling $A_{SF}$ produces a more robust fit to the long plateau exhibited in all data sources. Next, comparing panels (b) and (c) shows that while short-term predictions are broadly consistent, the spread of model forecasts become narrower. In particular, including data up to May 17, as in panel (c), enables the model to identify that the plateau is beginning to bend, in contrast to the model shown in panel (b), in which a continued plateau is not precluded. We investigate the predictive power of our model and calibration procedure in the next subsection.

Hospital and ICU occupancy as well as deaths related to COVID-19 exhibit a long plateau spanning from the beginning of April through at least mid May. This behavior is not just due to the fact that mitigation reduced $R_t$ to almost exactly one, but also because of the variance in when the lagging indicators respond to the rate of infection. Namely, while the various non-pharmaceutical interventions (NPIs) implemented in Illinois occurred on relatively short timescales (as can be seen in the sudden change of slope for the daily incidence of new infections in Fig. 2), the variance in the delays between when individuals become, e.g., symptomatic and then hospitalized, introduces spread in the indicators’ responses to changes in $R_t$. As an example, some portion of individuals infected before any mitigation takes place will continue to be admitted to the hospital well after mitigation occurs. Indeed, this variability compounds with subsequent transitions, such that daily deaths, being the final indicator, exhibit the most gradual change in incidence rate. Our model’s generality to arbitrary delay distributions makes it particularly well-suited to accurately capture this effect.

**B. Robustness of predictions**

In order to explore the predictive capabilities of the model, we present a series of benchmark simulations to compare the predictions of models calibrated with increasingly recent data. In Fig. 3 we show the fits to hospital beds occupied, ICU beds occupied, daily hospital deaths, and daily total deaths in the entire state of Illinois, cal-

![FIG. 2. Fits and predictions of our model of the entire state of Illinois under the continuation of the Stay-at-Home order and social distancing measures, resulting from parameter inference which (a) fixes $A_{SF} = 0.2$ and calibrates to data through April 20, 2020, (b) samples $A_{SF}$ and calibrates to data through April 20, 2020, and (c) samples $A_{SF}$ and calibrates to data through May 17, 2020. In each case, the data used for calibration is denoted by crosses, while data from later dates (open circles) allow a comparison of model predictions with subsequent real world observations. Each panel’s vertical line marks the end of data used for calibration. Solid curves denote median model predictions at a given time, while the shaded regions denote the 68.4% (darker shading) and 95.6% (lighter shading) confidence intervals of a particular output. We depict the daily incidence of new infections (green, solid), the number of occupied hospital beds by confirmed or tentative COVID-19 patients (purple, dashed), the number of ICU beds occupied by confirmed COVID-19 patients (orange, dot-dashed), and total daily deaths of COVID-19 patients (light blue, dotted). We remove reporting artifacts by plotting daily death data smoothed by a 7-day running average.](https://doi.org/10.1101/2020.06.03.20120691)
As expected, simulations with earlier terminal calibration dates generate forecasts with larger, less restrictive confidence intervals: with data from only the earliest stages of the epidemic, neither continued exponential growth nor successful suppression of infections due to mitigation can be ruled out. Between April 1 and April 8, however, ICU occupation stopped growing exponentially, thereby providing the first indicator by which the model can infer the effect of mitigation. Indeed, even the April 8 forecast anticipates the subsequent flattening in the daily deaths curve. Later forecasts (e.g., that of April 20) remain consistent with the April 8 model, while also favoring a continuation of the plateau over a more rapid decline in use of hospital resources and deaths. Finally, the May 3 model is largely consistent with the April 20 one, but begins to project a slight decline that agrees with the new data. This latest forecast should not be expected to lie strictly within the confidence interval of the previous, as any future changes in mitigation cannot be anticipated.

We also point out that the April 1 forecast for hospital occupation spans several orders of magnitude on any given day (as seen in panel (a) of Fig. 3). This is due in part to the lack of hospitalization data that could provide direct constraints, but is also an inevitable feature of a system which exhibits exponential growth dynamics. Furthermore, we hypothesize that the lack of hospitalization data before the beginning of the plateau is at least partially responsible for the April 1 forecast for ICU occupation and daily deaths being relatively unconstrained. Since hospitalizations serves as the earliest available indicator for the progression of the epidemic, we hypothesize that if it were supplied with this data before April 1, the model would have been able to discern that the data were no longer consistent with an exponentially-growing epidemic. This observation underscores the importance of rapid and reliable reporting of hospitalization data—or even better, robust and representative testing for positive cases—in the context of modeling epidemic dynamics.

The disappointingly short horizon of predictability for epidemic models when \( R_t > 1 \) shown here represents a fundamental limitation of forecasting, in much the same way that chaotic dynamics limits weather prediction, and this issue has been noticed in other independent studies \([35-40]\). However, the exponential sensitivity has a silver lining: small changes to transmission can have large impacts on the overall trajectory and fatality of the disease.

In summary, the model curves fitted after April 8, 2020, i.e., with data from the plateau, follow the trends of the data well. We conclude that the model can be characterized as semi-quantitative and that it is capable of capturing broad epidemic dynamics and fitting empirical data. In this sense, it can serve as a useful tool to make short term predictions that may be useful for planning purposes.
C. Regional modeling

To account for differences in the epidemic in different parts in the state, we simulate the epidemic trajectory in the four distinct Restore Illinois regions separately. Each of these “super-regions” is composed of multiple of the Emergency Medical Services (EMS) regions defined by the Illinois Department of Public Health (IDPH) [11]. The Northeast super-region includes the city of Chicago and its suburbs, EMS regions 7 through 11. The North-Central super-region contains EMS regions 1 and 2, the Central super-region EMS regions 3 and 6, and finally the Southern super-region comprises EMS regions 4 and 5. In the absence of detailed transportation data, we assume no population transfer between these super-regions, and so unlike, e.g., the model for the state of Georgia in Ref. [12] and Italy [23], our regional modeling is not a genuine metapopulation model for the state.

In Fig. 4 we show the fits and predictions of our model calibrated to data up to May 17, 2020 for each of these four regions. We report inferred model parameters in Table S2. Our median estimates of the basic reproduction number \( R_0 \) at the start of the epidemic are consistently above 1, ranging from 2.4 ± 0.16 for the Northeastern region including Chicago and its suburbs to 1.7 ± 0.16 for the Central region including the University of Illinois at Urbana-Champaign.

The per capita daily deaths and illnesses is at least ten-fold higher in Chicago and its suburbs compared to the downstate areas of Illinois. This is likely due to increased contact density in the upstate region, reflected by a higher initial \( R_0 \approx 2.3 \) compared to \( \approx 1.8 \) in the downstate regions, coupled with the fact that mitigation began earlier relative to the start of the epidemic in some downstate regions. In regions where the virus entered the population later, the epidemic had a shorter phase of unmitigated exponential growth.

The values of \( R_t \) corresponding to the post-mitigation basic reproduction number are very close to 1, reflecting the approximately constant number of hospital and ICU beds occupied by COVID-19 patients and daily deaths from COVID-19 in different super-regions in Illinois during much of April and May 2020.

D. Evaluation of parameter fits

In Fig. 5 we show a subset of the joint posterior probability distributions for model parameters relevant to the parameterization of the mitigation factor \( M(t) \) as specified above, fitting to data shown in Fig. 2. The correlations between some pairs of fitted parameters, e.g., between \( R_0 \) and the start date of the epidemic \( t_s \), are reflected in the ellipsoidal shape of the posteriors. This is sensible: the later the epidemic begins, the larger the basic reproduction number must be in order to fit the data.

In Table S2 we report the parameter values our model infers when fitting to data for different regions of the state and over different time ranges. We also report the effective reproduction numbers \( R_t \) as evaluated on May 1, 2020. On May 1, 2020, \( R_t \) appears to have barely dropped below unity, suggesting that mitigation efforts may have only marginally halted the exponential growth of the epidemic at that time.

E. Comparison with mobility data

While our model does not provide a microscopic description of social interactions and movement in the population, we may evaluate our fitted \( M(t) \) relative to social mobility indices derived from cell phone data [33, 34]. In the top panel of Fig. 6 we plot the time dependence of several mobility indices reported by Google [43] for the entire state of Illinois, measuring change in visits to destination points categorized as retail and recreation, grocery and pharmacy, parks, transit stations, and workplaces. The Unacast mobility data [44] is shown in bottom panel of Fig. 6 depicting an effective distancing metric and a measure of trips to so-called non-essential destinations.

Remarkably, although the model is supplied with no prior information on non-pharmaceutical interventions, the inferred dates and magnitude of mitigation agree with the start and end dates of the largest drop in both sets of mobility data. Comparing to the Google mobility data, our \( M(t) \) curve exhibits an amplitude, start date and end date consistent with indices corresponding to retail and recreation, transit stations and workplaces. On the other hand, parks and grocery and pharmacy show a more modest reduction which still matches the time frame of \( M(t) \). In the Unacast data, both metrics also appear to match the time-dependent change in \( M(t) \). Note that both datasets evidence increased movement at later dates. Because we here parameterize mitigation as a single transition, our fits to \( M(t) \) would not reproduce this recent increasing trend.

Our procedure is distinct compared to several previous efforts to incorporate mobility into models of COVID-19 dynamics, which either impose that changes in transmission coincide with known dates of non-pharmaceutical interventions, or scale \( R_t \) according to reductions in mobility [35, 40]. The fact that our model independently recovers a trend in mitigation consistent with mobility measures speaks to its flexibility and calibration procedure.

IV. WHAT-IF SCENARIOS

We now consider possible future scenarios and alternative historical scenarios in which non-pharmaceutical interventions are lifted or were never implemented at all. The former enables a model-based assessment of the risk of, e.g., lifting Stay-at-Home orders on a certain date, while the latter demonstrates the impact that previously-

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FIG. 4. Fits and predictions of our model under the baseline scenario with the Stay-at-Home order and social distancing maintained until October 1, 2020. The model is calibrated with data (crosses) through April 20, 2020 separately for each of the four super-regions of the state: (a) North-Central, (b) Northeast, (c) Central and (d) Southern. The data from later dates (open circles) were not used in our fits and allow a comparison of model predictions with real world observations. Solid lines of different denote the median model prediction at a given time. The shaded regions denote the 68.4% (darker shading) and 95.6% (lighter shading) confidence intervals, obtained as quantiles of an ensemble of forward simulations which sample the posterior distribution over model parameters. We depict the daily incidence of new infections (green, solid), the number of occupied hospital beds by confirmed or tentative COVID-19 patients (purple, dashed), the number of ICU beds occupied by confirmed COVID-19 patients (orange, dot-dashed), and total daily deaths of COVID-19 patients (light blue, dotted). We remove reporting artifacts by plotting daily death data smoothed by a 7-day running average.

implemented measures have already had on outcomes. Our analysis focuses on two key measures for guiding and justifying policy decisions: the stress imposed on the healthcare system and the death toll.

A. No Stay-at-Home order

We first investigate the trajectory of the COVID-19 epidemic in Illinois in the absence of any form of social distancing or mitigation measures, whether self-imposed or mandated by the government. We conclude that rate of hospital-bound deaths, ICU bed occupancy, and hospital bed occupancy would be higher than what actually took place by an order of magnitude or more, as shown in Fig. [1]. The Stay-at-Home order and self-imposed social distancing measures were clearly crucial to flattening the curve.

In Ref. [17] we made an early estimate of the ICU utilization in the city of Chicago under two scenarios: one in which the Stay-at-Home order was issued on March 20, 2020, and another in which the order was delayed by 20 days. Under the first scenario, the ICU utilization by COVID-19 patients never exceeded the number of ICU beds not occupied by other patients, while under the second scenario it exceeded ICU capacity by nearly a factor of ten. This example highlights the cost of mistiming in NPIs [48]. In spite of inevitable uncertainties associated with these early estimates, that work correctly identified the timing of the peak in ICU demand to happen on or around April 22, 2020. However, the magnitude of this peak was underestimated in this study, because the scenario assumed that post-mitigation value of $R_t = 0.9$ would be achieved by social distancing. In reality, the response of the population to the Stay-at-Home order in Chicago was somewhat weaker resulting in a larger value of $R_t$ and about a three-fold higher peak ICU bed occupancy than we had predicted.
B. Partial removal of Stay-at-Home order

The state of Illinois lifted its original Stay-at-Home order on May 30, 2020. In Fig. 8 we consider two scenarios for the lifting of Stay-at-Home orders for the entire state of Illinois. In the first scenario, mitigation effects are completely removed and $M(t) = 1$ for times $t$ after June 1, 2020. We also consider the more conservative case that mitigation recovers by 30% to $M(t) = M(t_1) + 0.3(1 - M(t_1))$ for $t$ after June 1, 2020. This second scenario assumes that a combination of self-regulation and remaining government-imposed mitigation measures, such as requiring wearing masks, banning large gatherings, etc., results in only a partial reduction of the effective mitigation factor.

The first scenario exhibits a substantial second wave, with rapid and strong peaks in all quantities occurring successively through the month of July. In the second, weaker (and perhaps more realistic) scenario, a second wave still occurs but does so later and with a reduced peak height. In this case, the peak demand for hospital and ICU beds and number of deaths are reduced.

An aggregated model of the entire state does not describe its heterogeneous population structure, which may be particularly important in forecasting beyond the lifting of the Stay-at-Home order. We now report separately the results of modeling the expiration of the Stay-at-Home (with a 30% reduction in mitigation) in each of the four aforementioned super-regions, with the caveat that we are unable to take into account possible transfers of people between the regions. As in Fig. 9 we first calibrate models using data through May 17, 2020, imposing again that mitigation recovers by 30% to $M(t) = M(t_1) + 0.3(1 - M(t_1))$ for $t$ after June 1, 2020.

In each super-region, a second wave is clearly visible, as all four populations still today have a significant number of infectious people at large. Although the Northeast region, which includes Cook County and metropolitan...
Chicago, has the biggest second wave in absolute numbers, its relative impact on the epidemic trajectory is smaller merely because the epidemic has not declined to the same extent as the other three regions. Under the worst case scenario, the more sparsely populated Southern, Central, and North-Central regions have relatively larger second waves because the epidemic as of yet is relatively less active in those regions compared to the Northeastern region, which includes Chicago and its suburbs.

We note that the magnitude of the second wave may be containable if rapid and efficient testing, contact tracing, and isolation mitigation strategies are employed \[49, 50\]. Following standard protocols \[51\], we estimate that even if purely manual contact tracing is employed for all three stages of tracing (case identification, tracing, and follow-up), the number of contact tracers required is approximately 8.3 times the daily number of new cases identified. A considerable reduction in workforce and an increase in efficiency can be obtained by electronic measures. Nevertheless, the potential magnitude of the second wave in this scenario suggests that contact tracing will be challenging and require extraordinary resources to execute.

V. DISCUSSION

Modeling plays an important role in the societal response to the COVID-19 pandemic, and a variety of approaches are used to inform public health policy, guide resource allocation, and plan non-pharmaceutical interventions \[52\]. The present study of the spread of COVID-19 in Illinois reveals both the strengths and limitations of modeling, and provides potentially actionable insights into the future spread of the disease. We begin with some technical points and best practices that we have developed during our work.

Model calibration: Our analysis highlights the importance of choosing appropriate data with which to calibrate models, and to perform calibration with precision. Due to the large number of parameters that inevitably enter epidemiological models, calibration requires parameter inference in a high dimensional space with strong potential for improper fits resulting from failure to reach global optima. Although the MCMC methods we use are computationally intensive, they are relatively efficient in exploring high
dimensional, multi-modal distributions, and converge to well-behaved global posterior probability distributions. Bayesian inference enables the incorporation of previous studies (e.g., meta-analyses) to provide reasonable priors on parameters which are poorly constrained by the available data. As an example, although the data we calibrate to does not constrain the prevalence of the infection, we systematically account for this uncertainty by informing our prior on the infection-fatality rate (IFR) from serological studies ([32]). The IFR is an important variable in terms of disease outcomes, and so model predictions must systematically account for the uncertainty in this variable.

In our analysis, we have taken data at its face value. A more thorough analysis could account for differences in the trustworthiness of data, e.g., programmatically dealing with uncertainties associated with classification of early hospital admissions as either COVID-positive or under investigation. Such an approach might also be able to consider the number of individuals who test positive for the virus. Furthermore, because we do not explicitly treat underreporting, data from early in the epidemic may be biased low.

**Error estimation:** The MCMC procedure generates a complex, high dimensional probability distribution that may be sampled to estimate future epidemic trajectories. While one might be tempted to simply generate the maximum likelihood trajectory for forward (in time) simulation, this can be misleading. The probability distribution of trajectories may have a maximum likelihood trajectory that is favored only slightly above other trajectories yet is noticeably different from the mean or median estimator. We thus sample trajectories forward in time, and at each time point we evaluate the median and confidence intervals of outputs. Although the curves we depict do not correspond to a trajectory that would be realised in practice, together with confidence intervals, they provide a meaningful description of the range of forecast results.

**Robustness:** In order to ascertain the predictive power of our model, we assessed to what extent it was able to make predictions beyond the range of data to which it had been calibrated. We first considered a rather severe test: how far in advance can the model predict the abrupt flattening of the epidemic curves that occurred after April 10, 2020? Unsurprisingly, the answer here was not particularly encouraging because the curves dramatically switch from exponential growth to a phase of much slower variation or plateau. We were only able to fit daily death and ICU occupancy data before the flattening, since hospitalization data was not available until mid-April. As a result, none of the information feeding into the model dynamics were able foreshadow the onset of the plateau.

Nevertheless, such self-consistency checks are important validations of the modeling process, and should be attempted if there are early enough data available. Encouragingly, the range of our model estimates decreased...
in a hierarchical and consistent manner, with projections from earlier points in time bounding later projections. Of course, it is not possible for our model to predict future changes to the strength of mitigation. Furthermore, our mitigation model only implements a single event and thus cannot account for future short term changes. Real world considerations, such as holidays and quarantine fatigue, would be inconsistent with our mitigation model approximations are frequently made [\cite{15}].

Declining more rapidly, due to a combination of social distancing measures on actual population movement, especially since its effects are likely also relevant for COVID-19 [\cite{55}]. Similarly, we do not account for heterogeneities in the population structure. Such features may accelerate the onset of herd immunity which in turn decreases $R_t$. These differences have the potential to decrease the severity of the second wave and may enable more efficient containment. We defer a treatment of these effects to future work.

Relaxing mitigation: Our simulations suggest that it is too soon to lift all social distancing and mitigation restrictions, as the significant number of currently-infectious individuals would make a second wave inevitable. The dynamics of a second wave and the approach to herd immunity may be crucially sensitive to effects beyond a mean-field description. For example, we do not account for super-spreader events which have played a major role in the spread of SARS and MERS [\cite{9, 10, 11, 13}] and are likely also relevant for COVID-19 [\cite{55}]. Similarly, we do not account for heterogeneities in the population structure. Such features may accelerate the onset of herd immunity which in turn decreases $R_t$. These differences have the potential to decrease the severity of the second wave and may enable more efficient containment. We defer a treatment of these effects to future work.

Additional limitations: We end with a brief discussion of additional limitations. First, the importance of spatial structure, heterogeneities in population susceptibility, and social network structure are well-appreciated in the literature [\cite{2, 12, 15}]. We plan to investigate methods to model these effects and their impact on our results in future work. In addition, important sources of error in our existing model include the unknown impact of seasonal forcing, the discreteness of populations, and the effect of super-spreader events and behavioral response.

In our initial modeling [\cite{17}], we used seasonal forcing with $A_{SF} = 0.2$ because similar effects had been documented for historical coronaviruses [\cite{19}]. Because seasonal forcing varies slowly with time, it remains difficult to verify this assumption with the observables we consider. Nevertheless, our parameter inference does not exhibit strong evidence for this level of seasonal forcing; the role of climate in the early stages of epidemics is a question of active investigation [\cite{56, 57}]. Furthermore, non-zero values for $A_{SF}$ do not necessarily ascribe an equivalent seasonal modulation to the disease’s infectivity.

In addition, we wish to comment on the reported confidence intervals obtained from parameter inference for both stochastic and deterministic epidemic models [\cite{58}], because these can depend on whether or not the model calibrations are performed for raw data or cumulative data. Generally speaking the estimated intervals are unrealistically small when models are fit to cumulative data [\cite{58}], with stochastic models giving slightly larger intervals. Our calculations are calibrated to raw data not cumulative data, and so we do not expect the uncertainties in general to be estimated inappropriately. Regardless, any deterministic model of the epidemic trajectory will be inappropriate when few individuals are infected, in spite of apparent certainty in posteriors. Thus, in a regime
where the deterministic model is not even appropriate as a first approximation, i.e., small populations, the estimate of uncertainties will not be a good indicator of the inapplicability of the deterministic model. Moreover, it is well-known in ecology that the discreteness of populations—the fact that individuals are quantized and that birth-death processes are discrete—leads to important qualitative phenomena ranging from population cycles \[59\] to noise-induced pattern formation \[60, 61\]. These effects are particularly important when numbers are small in the early and late stages of the epidemic because our mean-field model is incapable of representing the extinction state, i.e., when the number of infectious individuals drops below one. Once the epidemic is extinct in a particular region, it can only re-emerge due to migration events, e.g., a super-spreader event like when university students return to campus. In this regime, a prudent regional health department uses contact tracing to contain outbreaks. Such mechanisms are not represented in our modeling.

The third major limitation is that modeling an epidemic is very different from modeling a physical system, even one as complex as a weather pattern. The transmission of an infectious disease involves a collaboration between the virus and the host population: the host population alters its behavior in response to its awareness of epidemic progress, leading to policy steps that may increase or decrease transmission, and self-regulation of social distancing by susceptible and vulnerable populations. Thus, it is important to emphasize that predictions can easily be invalidated due to subsequent human actions that cannot be anticipated, and will be impossible to model precisely.

VI. CONCLUSIONS

In this paper, we have presented a mathematical model and computational framework for recapitulating the COVID-19 epidemic. This model may be used to infer values for the parameters that drive and represent the model and computational framework for recapitulating the epidemic. The resulting highly-constrained and quantitative narrative of the epidemic is a useful tool to inform scenarios for sustainable monitoring and control of the epidemic.

CODE AVAILABILITY

The model and calibration framework described above have been implemented in the open source Python 3 \[62\] package `pydemic`. The source code for `pydemic` is freely available online at \texttt{https://github.com/uiuc-covid19-modeling/pydemic}. This work made use of NumPy \[63\], SciPy \[64\], pandas \[65\], emcee \[66\], corner.py \[66\], and Matplotlib \[67\].

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[1] All executive orders related to COVID-19 issued by the State of Illinois Governor JB Pritzker are listed here: \texttt{https://www2.illinois.gov/government/executive-orders}. The timeline of COVID-19 mitigation in Illinois is summarized at: \texttt{https://en.wikipedia.org/wiki/COVID-19_pandemic_in_Illinois#Government_response}.

[2] M. J. Keeling and P. Rohani, \textit{Modeling infectious diseases in humans and animals}. Princeton University Press, 2011.

[3] C. J. L. Murray, “Forecasting COVID-19 impact on hospital bed-days, ICU-days, ventilator-days and deaths by US state in the next 4 months,” \textit{medRxiv}, p. 2020.03.27.20043752, 2020.

[4] J. Ma, “Estimating epidemic exponential growth rate and basic reproduction number,” \textit{Infectious Disease Modelling}, vol. 5, pp. 129 – 141. 2020. [Online]. Available: \texttt{http://www.sciencedirect.com/science/article/pii/S2468042719300491}.
[5] J. T. Wu, K. Leung, and G. M. Leung, “Nowcasting and forecasting the potential domestic and international spread of the 2019-ncov outbreak originating in wuhan, china: a modelling study,” The Lancet, vol. 395, no. 10225, pp. 689–697, 2020.
[6] C. Fraser, “Estimating individual and household reproduction numbers in an emerging epidemic,” PLoS One, vol. 2, no. 8, p. e758, 2007. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC17712406
[7] G. Chowell, “Fitting dynamic models to epidemic outbreaks with quantified uncertainty: a primer for parameter uncertainty, identifiability, and forecasts,” Infectious Disease Modelling, vol. 2, no. 3, pp. 379–398, 2017.
[8] J. T. Wu, K. Leung, M. Bushman, N. Kishore, R. Niedus, P. M. de Salazar, B. J. Cowling, M. Lipsitch, and G. M. Leung, “Estimating clinical severity of COVID-19 from the transmission dynamics in Wuhua, China,” Nat Med, vol. 26, no. 4, pp. 506–510, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC32284616
[9] C. Viboud, O. N. Bjornstad, D. L. Smith, L. Simonsen, M. A. Miller, and B. T. Grenfell, “Synchrony, waves, and spatial hierarchies in the spread of influenza,” Science, vol. 312, no. 5772, pp. 447–451, 2006.
[10] J. O. Lloyd-Smith, S. J. Schreiber, P. E. Kopp, and W. M. Getz, “Superspreading and the effect of individual variation on disease emergence,” Nature, vol. 438, no. 7066, pp. 355–9, 2005. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC16292310
[11] M. Small, C. Tse, and D. M. Walker, “Super-spreaders and the rate of transmission of the sars virus,” Physica D: Nonlinear Phenomena, vol. 215, no. 2, pp. 146–158, 2006.
[12] S. Bansal, B. T. Grenfell, and L. A. Meyers, “When individual behaviour matters: homogeneous and network models in epidemiology,” Journal of the Royal Society Interface, vol. 4, no. 16, pp. 879–891, 2007.
[13] Y. Kim, H. Ryu, and S. Lee, “Agent-based modeling for super-spreading events: A case study of mers-cov transmission dynamics in the republic of korea,” International Journal of Environmental Research and Public Health, vol. 15, no. 11, p. 2369, 2018.
[14] Z. Dezso and A.-L. Barabasi, “Halting viruses in scale-free networks,” Physical Review E, vol. 65, no. 5, p. 055103, 2002.
[15] K. Rock, S. Brand, J. Moir, and M. J. Keeling, “Dynamics of infectious diseases,” Reports on Progress in Physics, vol. 77, no. 2, p. 026602, 2014.
[16] R. Pastor-Satorras, C. Castellano, P. Van Mieghem, and A. Vespignani, “Epidemic processes in complex networks,” Reviews of Modern Physics, vol. 87, no. 3, p. 925, 2015.
[17] W. O. Kermack and A. G. McKendrick, “A contribution to the mathematical theory of epidemics,” Proceedings of the Royal Society of London. Series A, Containing papers of a mathematical and physical character, vol. 115, no. 772, pp. 700–721, 1927.
[18] J. Wallinga and M. Lipsitch, “How generation intervals shape the relationship between growth rates and reproductive numbers,” Proceedings of the Royal Society B: Biological Sciences, vol. 274, no. 1609, pp. 599–604, 2006.
[19] R. A. Neher, R. Dyrdak, V. Drueelle, E. B. Hodcroft, and J. Albert, “Potential impact of seasonal forcing on a SARS-CoV-2 pandemic,” Swiss Medical Weekly, vol. 150, no. 1112, 2020.
[20] A. Smirnova, L. deCamp, and G. Chowell, “Forecasting epidemics through nonparametric estimation of time-dependent transmission rates using the SEIR model,” Bulletin of Mathematical Biology, vol. 81, no. 11, pp. 4343–4365, 2019.
[21] C. C. Ku, T.-C. Ng, and H.-H. Lin, “Epidemiological Benchmarks of the COVID-19 Outbreak Control in China after Wuhan’s Lockdown: A Modelling Study with An Empirical Approach,” SSRN Electronic Journal, 2020.
[22] R. H. Mena, J. X. Velasco-Hernandez, N. B. Mantilla-Beniers, G. A. Carranco-Sapiens, L. Benet, D. Boyer, and I. P. Castillo, “Using the posterior predictive distribution to analyse epidemic models: COVID-19 in Mexico City,” arXiv preprint arXiv:2005.02294, 2020.
[23] M. Gatto, E. Bertuzzo, L. Mari, S. Miccoli, L. Carraro, R. Casagrandi, and A. Rinaldo, “Spread and dynamics of the COVID-19 epidemic in Italy: Effects of emergency containment measures,” Proceedings of the National Academy of Sciences, vol. 117, no. 19, pp. 10484–10491, 2020.
[24] H. Nishiura, N. M. Linton, and A. R. Akhmetzhanov, “Serial interval of novel coronavirus (COVID-19) infections,” International Journal of Infectious Diseases, vol. 93, pp. 284–286, 2020.
[25] Z. Du, X. Xu, Y. Wu, L. Wang, B. J. Cowling, and L. A. Meyers, “Serial Interval of COVID-19 among Publicly Reported Confirmed Cases,” Emerg Infect Dis, vol. 26, no. 6, pp. 2020.02.19.2002542, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC32191273
[26] S. A. Lauer, K. H. Grantz, Q. Bi, P. K. Jones, Q. Zheng, H. R. Meredith, A. S. Azman, N. G. Reich, and J. Lessler, “The Incubation Period of Coronavirus Disease 2019 (COVID-19) From Publicly Reported Confirmed Cases: Estimation and Application,” Annals of Internal Medicine, vol. 172, no. 9, p. 577, 2020.
[27] N. M. Linton, T. Kobayashi, Y. Yang, K. Hayashi, A. R. Akhmetzhanov, S.-m. Jung, B. Yuan, R. Kinoshita, and H. Nishiura, “Incubation Period and Other Epidemiological Characteristics of 2019 Novel Coronavirus Infections with Right Truncation: A Statistical Analysis of Publicly Available Case Data,” Journal of Clinical Medicine, vol. 9, no. 2, p. 538, 2020.
[28] R. Verity, L. C. Okell, I. Dorigatti, P. Winskill, C. Whittaker, N. Imai, G. Cuomo-Dannenburg, H. Thompson, P. G. T. Walker, H. Fu, A. Dighe, J. T. Griffin, M. Baguelin, S. Bhatia, A. Boonyasiri, A. Cori, Z. Cucunuba, R. FitzJohn, K. Gaythorpe, W. Green, A. Hamlet, W. Hinsley, D. Laydon, G. Nedjati-Gilani, S. Riley, S. van Elsland, E. Volz, H. Wang, Y. Wang, X. Xi, C. A. Donnelly, A. C. Ghani, and N. M. Ferguson, “Estimates of the severity of coronavirus disease 2019: a model-based analysis,” Lancet Infect Dis, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC32240634
[29] P. K. Bhatraju, B. J. Ghasssemieh, M. Nichols, R. Kim, K. R. Jerome, A. K. Nalla, A. L. Greninger, S. Pipavath, M. M. Wurfel, L. Evans, P. A. Kritek, T. E. West, A. Luks, A. Gerbino, C. R. Dale, J. D. Goldman, S. O’Mahony, and C. Mikacenic, “Covid-19 in Critically Ill Patients in the Seattle Region - Case Series,” N Engl J Med, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pmc/articles/PMC32227758
[30] X. Yang, Y. Yu, J. Xu, H. Shu, J. Xia, H. Liu, Y. Wu, L. Zhang, Z. Yu, M. Fang, T. Yu, Y. Wang, S. Pan, X. Zou, S. Yuan, and Y. Shang, “Clinical course and outcomes of critically ill patients with SARS-CoV-2 pneumonia in Wuhan, China: a single-centered, retrospective, observa-

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tional study,” The Lancet Respiratory Medicine, vol. 8, no. 5, pp. 475–481, 2020.

31 “ICNARC report on COVID-19 in critical care, 08 May 2020,” 2020. [Online]. Available: https://www.icnarc.org/Our-Audit/Audits/Cmp/Reports

32 G. Meyerowitz-Katz and L. Merone, “A systematic review and meta-analysis of published research data on COVID-19 infection-fatality rates,” medRxiv, p. 2020.05.03.20089854, 2020.

33 D. Foreman-Mackey, W. Farr, M. Sinha, A. Archibald, D. Hogg, J. Sanders, J. Zuntz, P. Williams, A. Nelson, M. de Val-Borro, T. Erhardt, I. Pashchenko, and O. Pla, “emcee v3: A Python ensemble sampling toolkit for affine-invariant MCMC,” The Journal of Open Source Software, vol. 4, no. 43, p. 1864, Nov. 2019.

34 C. J. F. ter Braak and J. A. Vrugt, “Differential Evolution Markov Chain with snooker updater and few chains,” Statistics and Computing, vol. 18, no. 4, pp. 435–446, Dec 2008. [Online]. Available: https://doi.org/10.1007/s11222-008-9104-9

35 C. J. F. ter Braak, “A Markov Chain Monte Carlo version of the genetic algorithm Differential Evolution: easy Bayesian computing for real parameter spaces,” Statistics and Computing, vol. 16, no. 3, pp. 239–249, Sep 2006. [Online]. Available: https://doi.org/10.1007/s11222-006-9769-1

36 D. Farr, V. Kalogerera, and E. Luijten, “A more efficient approach to parallel-tempered markov-chain monte carlo for the highly structured posteriors of gravitational-wave signals,” Physical Review D, vol. 90, no. 2, p. 024014, 2014.

37 Data were downloaded from https://www.dph.illinois.gov/covid19/covid19-statistics.

38 I. Korolev, “Identification and Estimation of the ICNARC report on COVID-19 in critical care, 08 May 2020,” 2020, https://www.icnarc.org/Our-Audit/Audits/GA

39 M. Castro, S. Ares, J. A. Cuesta, and S. Manrubia, “Predictability: Can the turning point and end of an expanding epidemic be precisely forecast?” arXiv, pp. arXiv-2004, 2020.

40 W. C. Roda, M. B. Varughese, D. Han, and M. Y. Li, “Why is it difficult to accurately predict the COVID-19 epidemic?” Infectious Disease Modelling, vol. 5, p. 271, 2020.

41 See map at https://www.dph.illinois.gov/sites/default/files/resources/ems-regions-map.pdf.

42 S. J. Beckett, M. Dominguez-Mirazo, S. Lee, C. Andris, and J. S. Weitz, “Spread of COVID-19 through Georgia, USA. Near-term projections and impacts of social distancing via a metapopulation model.” [Online]. Available: https://github.com/WeitzGroup/MAGEmodel_covid19_GA/blob/master/Report/GA_COVID19_assessment_21Apr2020.pdf

43 https://www.blog.google/technology/health/covid-19-community-mobility-reports?hl=en

44 https://www.unacast.com/post/rounding-out-the-social-distancing-scoreboard

45 S. Flaxman, S. Mishra, A. Gandy, H. Unwin, H. Coupland, T. Mellan et al., “Report 13. Estimating the number of infections and the impact of non-pharmaceutical interventions on COVID-19 in 11 European countries. Imperial College London, 2020,” 2020. [Online]. Available: https://doi.org/10.25561/7731

46 H. J. T. Unwin, S. Mishra, V. Bradly, A. Gandy, M. Vollmer, T. Mellan, H. Coupland, K. Ainslie, C. Whittaker, J. Ish-Horowicz, S. Filippi, X. Xi, M. Monod, O. Ratmann, M. Hutchinson, F. Valha, H. Zhu, I. Hawryluk, P. Milton, M. Baguelin, A. Boonyasiri, N. Brazeau, L. Cattarino, G. Charles, L. V. Cooper, Z. Cucunuba, G. CuomoDannenburg, B. Djaafara, I. Dorigatti, O. J. Eales, J. Eaton, S. van Elsland, R. Fitzjohn, K. Gaythorpe, W. Green, T. Hallett, W. Hinsley, N. Imai, B. Jeffrey, E. Knock, D. Laydon, J. Lees, G. Nedjati-Gilani, P. Nouvellet, L. Okell, A. Ower, K. V. Parag, I. Siveroni, H. A. Thompson, R. Verity, P. Walker, C. Walters, Y. Wang, O. J. Watson, L. Whitlles, A. Ghani, N. M. Ferguson, S. Riley, C. A. Donnelly, S. Bhat, and S. Flaxman, “Report 23: State-level tracking of COVID-19 in the United States WHO Collaborating Centre for Infectious Disease Modelling MRC Centre for Global Infectious Disease Analytics,” 2020.

47 S. Maslov and N. Goldenfeld, “Window of Opportunity for Mitigation to Prevent Overflow of ICU capacity in Chicago by COVID-19,” medRxiv, 2020. [Online]. Available: https://www.medrxiv.org/content/early/2020/03/24/2020.03.20.20040048

48 D. H. Morris, F. W. Rossine, J. B. Plotkin, and S. A. Levin, “Optimal, near-optimal, and robust epidemic control,” arXiv preprint arXiv:2004.02209, 2020.

49 J. Hellewell, S. Abbott, A. Gimma, N. I. Bosse, C. I. Jarvis, T. W. Russell, J. D. Munday, A. J. Kucharski, and R. M. Eggo, “Feasibility of controlling COVID-19 outbreaks by isolation of cases and contacts,” The Lancet Global Health, 2020.

50 L. Ferretti, C. Wymant, M. Kendall, L. Zhao, A. Nurtay, L. Abeler-Dorner, M. Parker, D. Bonsall, and C. Fraser, “Quantifying SARS-CoV-2 transmission suggests epidemic control with digital contact tracing,” Science, p. eabb6936, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pubmed/32234805

51 Fitzhugh Mullan Institute for Health Workforce Equity, George Washington University, “Contact tracing workforce estimator,” https://www.gwhwi.org/estimator-613404.html.

52 I. Holm Dahl and C. Buckee, “Wrong but Useful — What Covid-19 Epidemiologic Models Can and Cannot Tell Us,” New England Journal of Medicine, 2020. [Online]. Available: https://doi.org/10.1056/NEJMp2016822

53 K. D. Stårk, G. Regula, J. Hernandez, L. Knopf, K. Fuchs, R. S. Morris, and P. Davies, “Concepts for risk-based surveillance in the field of veterinary medicine and veterinary public health: review of current approaches,” BMC health services research, vol. 6, no. 1, p. 20, 2006.

54 A. Foddai, A. Lindberg, J. Lubroth, and J. Ellis-Iversen, “Surveillance to improve evidence for community control decisions during the COVID-19 pandemic—Opening the animal epidemic toolbox for Public Health,” One Health, vol. 9, p. 100130, 2020.

55 Y. Liu, R. M. Eggo, and A. J. Kucharski, “Secondary attack rate and superspreading events for SARS-CoV-2,” Lancet, vol. 395, no. 10227, p. e47, 2020. [Online]. Available: https://www.ncbi.nlm.nih.gov/pubmed/32113505

56 K. S. Raines, S. Doniach, and G. Bhanot, “The transmission of sars-cov-2 is likely modulated by temperature and by relative humidity,” medRxiv, 2020. [Online]. Available: https://www.medrxiv.org/content/
R. E. Baker, W. Yang, G. A. Vecchi, C. J. E. Metcalf, and B. T. Grenfell, “Susceptible supply limits the role of climate in the covid-19 pandemic,” medRxiv, 2020. [Online]. Available: https://www.medrxiv.org/content/early/2020/05/26/2020.05.23.20111278

A. A. King, M. Domenech de Celis, F. M. Magpantay, and P. Rohani, “Avoidable errors in the modelling of outbreaks of emerging pathogens, with special reference to Ebola,” Proceedings of the Royal Society B: Biological Sciences, vol. 282, no. 1806, p. 20150347, 2015.

A. J. McKane and T. J. Newman, “Predator-prey cycles from resonant amplification of demographic stochasticity,” Physical Review Letters, vol. 94, no. 21, p. 218102, 2005.

T. Butler and N. Goldenfeld, “Robust ecological pattern formation induced by demographic noise,” Physical Review E, vol. 80, no. 3, p. 030902, 2009.

D. Karig, K. M. Martini, T. Lu, N. A. DeLateur, N. Goldenfeld, and R. Weiss, “Stochastic Turing patterns in a synthetic bacterial population,” Proceedings of the National Academy of Sciences, vol. 115, no. 26, pp. 6572–6577, 2018.

G. Van Rossum and F. L. Drake, Python 3 Reference Manual. Scotts Valley, CA: CreateSpace, 2009.

T. E. Oliphant, A guide to NumPy. Trelgol Publishing USA, 2006, vol. 1.

D. Foreman-Mackey, “corner.py: Scatterplot matrices in python,” The Journal of Open Source Software, vol. 24, 2016. [Online]. Available: http://dx.doi.org/10.5281/zenodo.45906

J. D. Hunter, “Matplotlib: A 2d graphics environment,” Computing in Science & Engineering, vol. 9, no. 3, pp. 90–95, 2007.

The Novel Coronavirus Pneumonia Emergency Response Epidemiology Team, “The Epidemiological Characteristics of an Outbreak of 2019 Novel Coronavirus Diseases (COVID-19) — China, 2020,” China CDC Weekly, vol. 2, p. 113, 2020. [Online]. Available: http://weekly.chinacdc.cn/article/id/e53946e2-c6c4-41e9-9a9b-fea8d9a851

K. Mizumoto, K. Kagaya, A. Zarebski, and G. Chowell, “Estimating the asymptomatic proportion of coronavirus disease 2019 (COVID-19) cases on board the Diamond Princess cruise ship, Yokohama, Japan, 2020,” Eurosurveillance, vol. 25, no. 10, 2020. [Online]. Available: https://www.eurosurveillance.org/content/10.2807/1560-7917.ES.2020.25.10.2000180

H. Nishiura, T. Kobayashi, T. Miyama, A. Suzuki, S. Jung, K. Hayashi, R. Kinoshita, Y. Yang, B. Yuan, A. R. Akhmetzhanov, and N. M. Linton, “Estimation of the asymptomatic ratio of novel coronavirus infections (COVID-19),” 2020. [Online]. Available: https://www.medrxiv.org/content/early/2020/02/17/2020.02.03.20020248

[70] Data were downloaded from https://data.un.org/
SUPPLEMENTARY MATERIAL

We detail the parameterization of our age-dependent severity model below. As noted in Section I A, we track the number of individuals in different age groups separately, and thus we specify the fiducial transition probabilities for each age group independently. We further define an overall scaling prefactor $p_x$ that governs the final transition probability $p_{x,i}$ as the product of the fiducial rate and the prefactor. Our fiducial transition rates $p_{x,i}/p_x$ are drawn from Ref. [28, 68–70].

In Table S1 we list the age-dependent values for the probabilities that: infected individuals experience symptoms $p_{\sigma,i}/p_{\sigma}$, symptomatic individuals are hospitalized $p_{h,i}/p_{h}$, hospitalized patients enter the ICU $p_{c,i}/p_{c}$, and ICU patients expire $p_{d,i}/p_{d}$. We also list the relative age distribution of the population in the United States, which we source from the UN [71]. As specified in Table I, we sample over the $p_c$ and $p_d$ scale factors.

TABLE S1. Table of age-specific parameters, including the age distribution $w_i$ and the various probabilities of transitioning between various states in our model. We present the unscaled distribution $p_{x,i}/p_{x}$, where $p_x$ denotes the overall scaling which is sampled during parameter inference (or whose value is otherwise set as described in the text).

| Age Group | $w_i$ | $p_{\sigma,i}/p_{\sigma}$ | $p_{h,i}/p_{h}$ | $p_{c,i}/p_{c}$ | $p_{d,i}/p_{d}$ |
|-----------|-------|--------------------------|-----------------|-----------------|-----------------|
| [0, 10]   | 0.120004 | 0.057 | 0.001 | 0.05 | 0.3 |
| [10, 20]  | 0.127891 | 0.054 | 0.003 | 0.05 | 0.3 |
| [20, 30]  | 0.139256 | 0.294 | 0.012 | 0.05 | 0.3 |
| [30, 40]  | 0.134948 | 0.668 | 0.032 | 0.05 | 0.3 |
| [40, 50]  | 0.121898 | 0.614 | 0.049 | 0.05 | 0.3 |
| [50, 60]  | 0.12725  | 0.83 | 0.102 | 0.063 | 0.3 |
| [60, 70]  | 0.116278 | 0.99 | 0.166 | 0.122 | 0.4 |
| [70, 80]  | 0.0727565 | 0.995 | 0.243 | 0.274 | 0.4 |
| [80, \infty] | 0.0397193 | 0.999 | 0.273 | 0.432 | 0.5 |

Because the data to which we calibrate does not constrain the symptomatic population, we cannot observe $p_h$ and so we fix it to one. We force our model to produce a given infection fatality ratio by setting $p_{\sigma}$ to

$$p_{\sigma} = \frac{\text{IFR}}{\sum_i w_i (p_{\sigma,i}/p_{\sigma}) p_{c,i} p_{h,i} p_{d,i} F_{\text{tot}}},$$

(S1)

where the value for $p_{\sigma,i}/p_{\sigma}$ on the right hand side of the equation is taken first from Table S1. This equation is valid if the initial infected population is distributed in proportion to $w_i$.

In Table S2 we summarize the posterior probability distribution for all sample parameters enumerated in Table I. Figure S1 shows joint posterior distributions for all pairs over the complete set of parameters of our model fitted to all-state data up to May 17, 2020 as shown in the bottom panel of Fig. 2.
TABLE S2. Table of inferred model parameters for disease severity and the time dependence of mitigation effects. Mitigation was modeled with a piecewise Hermite cubic interpolating polynomial as described in Section I A. Each column reports median error bounds reported by the algorithm. In addition, we report the (derived) values and uncertainties of parameter values from the MCMC algorithm for the different model fits along with the largest of the upper and lower one-sigma bounds for each model as evaluated on May 1, 2020. The column headers specify the modeled region of Illinois and the inclusive end date of the calibration data.

| Parameter | Illinois (5/17) | Illinois (4/20) | Northeastern (5/17) | North-Central (5/17) | Central (5/17) | Southern (5/17) |
|-----------|-----------------|-----------------|---------------------|----------------------|----------------|-----------------|
| $R_0$     | 2.2 ± 0.26      | 2.2 ± 0.25      | 2.3 ± 0.28          | 1.6 ± 0.38           | 1.6 ± 0.4      | 1.6 ± 0.33      |
| $t_s$     | Feb 15 ± 3.92   | Feb 14 ± 4.24   | Feb 16 ± 3.73       | Feb 16 ± 7.82        | Feb 18 ± 8.25  | Feb 17 ± 8.40   |
| $t_0$     | Mar 9 ± 4.13    | Mar 10 ± 4.13   | Mar 9 ± 4.04        | Mar 8 ± 5.71         | Mar 8 ± 6.08   | Mar 11 ± 7.62   |
| $t_1$     | Mar 20 ± 2.94   | Mar 21 ± 3.28   | Mar 20 ± 3.01       | Mar 24 ± 6.04        | Mar 25 ± 6.58  | Apr 4 ± 5.53    |
| $M(t_1)$  | 0.48 ± 0.051    | 0.47 ± 0.048    | 0.45 ± 0.048        | 0.64 ± 0.12          | 0.61 ± 0.12    | 0.59 ± 0.099    |
| $R_0$ (May 1) | 0.94 ± 0.01 | 0.97 ± 0.037    | 0.94 ± 0.011        | 0.99 ± 0.02          | 0.95 ± 0.023   | 0.9 ± 0.027     |
| IFR       | 0.007 ± 0.0012  | 0.0071 ± 0.0012 | 0.007 ± 0.0012      | 0.007 ± 0.0012       | 0.007 ± 0.0012 | 0.007 ± 0.0012  |
| $\tau_h$  | 6.3 ± 2         | 6.2 ± 2         | 6.2 ± 2             | 6.1 ± 1.8            | 6.2 ± 1.8      | 6.9 ± 1.8       |
| $\sigma_h$| 2.3 ± 1.4       | 2.2 ± 1.6       | 2.4 ± 1.7           | 4.2 ± 1.9            | 4.2 ± 1.9      | 4.6 ± 1.7       |
| $\tau_{disch}$ | 7 ± 1.9 | 6.9 ± 1.9       | 7.1 ± 1.9           | 6.2 ± 1.7            | 6.6 ± 1.8      | 6.9 ± 1.9       |
| $\sigma_{disch}$ | 6.1 ± 1.8 | 5.7 ± 2         | 6.4 ± 1.7           | 3.5 ± 1.7            | 4.6 ± 1.9      | 5 ± 1.8         |
| $p_c$     | 0.61 ± 0.16     | 0.67 ± 0.18     | 0.62 ± 0.17         | 0.47 ± 0.14          | 0.32 ± 0.097   | 0.51 ± 0.14     |
| $\tau_e$  | 1.4 ± 0.097     | 1.7 ± 1.3       | 1.3 ± 0.93          | 3 ± 1.6              | 2.2 ± 1.5      | 2 ± 1.3         |
| $\sigma_e$| 2.2 ± 1.8       | 2 ± 1.8         | 2.3 ± 1.9           | 2.5 ± 1.6            | 2.5 ± 1.7      | 2.7 ± 1.7       |
| $p_d$     | 1.4 ± 0.15      | 1.3 ± 0.16      | 1.4 ± 0.16          | 1.6 ± 0.3            | 1.9 ± 0.25     | 1.9 ± 0.26      |
| $\tau_d$  | 8.8 ± 0.96      | 7.7 ± 1         | 8.8 ± 0.98          | 13 ± 2.1             | 8.9 ± 1.6      | 11 ± 1.4        |
| $\sigma_d$| 4.6 ± 1.5       | 3.7 ± 1.5       | 4.7 ± 1.6           | 9.2 ± 2.4            | 7 ± 2.7        | 6.6 ± 2.2       |
| $\tau_{rec}$ | 11 ± 2.3 | 12 ± 2.5        | 11 ± 2.3            | 12 ± 2.8             | 12 ± 2.8       | 12 ± 2.8        |
| $\sigma_{rec}$ | 6.8 ± 2.7 | 8.7 ± 2.9   | 6.9 ± 2.7           | 10 ± 2.8             | 10 ± 2.8       | 9.9 ± 2.9       |
| $F_{tot}$ | 1.4 ± 0.033     | 1.3 ± 0.06      | 1.4 ± 0.034         | 1.2 ± 0.14           | 1.6 ± 0.3      | 2.1 ± 0.28      |
| $\tau_{tot}$ | 2.9 ± 0.46 | 2 ± 0.53        | 2.8 ± 0.47          | 2.2 ± 0.88           | 2.3 ± 0.91     | 2.8 ± 0.88      |
| $\sigma_{tot}$ | 2.3 ± 0.88 | 1.9 ± 0.84      | 2.2 ± 0.86          | 2.1 ± 0.91           | 2 ± 0.92       | 1.9 ± 0.91      |
| $A_{SP}$  | 0.15 ± 0.03     | 0.06 ± 0.071    | 0.11 ± 0.035        | 0.13 ± 0.065         | 0.12 ± 0.07    | 0.13 ± 0.073    |
FIG. S1. Joint posterior distributions of pairs of the complete set of parameters of our model fitted to the all-state data up to May 17, 2020. The correlations between some pairs of fitted parameters such as, e.g., between $R_0$ and that start date of the epidemic are reflected in the ellipsoidal shape of the posteriors. This is an expanded version of Fig. 5.