Influence of Different Surface Pretreatments of Zirconium Dioxide Reinforced Lithium Disilicate Ceramics on the Shear Bond Strength of Self-Adhesive Resin Cement

Introduction

Due to optical characteristics which are in common with the natural tooth substance and good physical and mechanical properties, dental ceramic materials exhibit chemical stability and excellent biocompatibility with soft tissues, with low plaque adhesion.

Uvod

Dentalna keramika ima slična optička svojstva kao i prirodna zubna sustancija – kemijsku stabilnost, dobra fizikalna i mehanička svojstva te izvrsnu biokompatibilnost s mekim tkivima s niskom adhezijom plaka.
Zirconium oxide ceramic materials have excellent mechanical performances, such as high flexural strength (1.0-1.2 GPa) and toughness (7-8 MPa × m 0.5). Therefore, they are increasingly used in dental practice, especially in CAD/CAM technology (computer-aided design/computer-aided manufacturing). Zirconium oxide ceramics can be used to make all types of ceramic replacements (crowns, bridges, fixed partial dentures, etc.). The whole procedure, using CAD/CAM technology, is extremely practical and reliable. The zirconia-based core structure is veneered with zirconia veneering ceramics. Both the core and the veneering ceramic have a similar thermal expansion coefficient. In dental practice, clinicians often face a variety of challenges such as choosing the best rehabilitation material when a prosthetic restoration is required on two adjacent teeth — on one zirconium ceramic crown and the other veneer. For esthetic reasons, it would be desirable to use the same type of material, but almost no information is available about zirconia veneering ceramic materials, which have yet to be further explored.

The zirconia-reinforced lithium silicate (ZLS) consists of lithium-metasilicate (Li 2 SiO 3 ) glass-ceramic and 10% of zirconium dioxide (ZrO 2 ). Ultimately, the crystallization process leads to the fine-grained microstructure formation (Li 2 O–ZrO 2 –SiO 2 ). ZLS is also progressively used in CAD/CAM technology, thanks to its good mechanical properties and excellent esthetics. Good mechanical properties can be attributed to zirconium dioxide, and esthetics to glass-ceramics. ZLS can be etched and cemented with adhesive systems, while the same procedure cannot be applied to zirconia restorations. Researchers have proved that the fracture resistance of adhesively cemented, monolithic CAD/CAM fabricated ceramic crowns is remarkably higher compared to conventional cementation (1).

Ceramic restorations have become the “gold standard” for anterior teeth restorations. The shear bond strength of composite cement to previously both etched and silanated porcelain surface surpasses the cohesive porcelain strength. The bonding of composite cement with ceramics is performed in two different ways: mechanically, as a consequence of etching with hydrofluoric acid and the formation of micromechanical retention and chemically, utilizing silane. At the same time, its bonding to enamel is achieved only mechanically. Many researchers encourage porcelain silanization in order to obtain a much stronger connection compared to etching with hydrofluoric acid only, whilst the combination of both is suggested.

The Er: YAG laser acts by thermomechanical ablation vaporizing the water that constitutes the tissues. This vaporization causes an expansion followed by microexplosions, which produces the ejection of both organic and inorganic particles from tissues, promoting the appearance of a dentinal surface and open tubules and without smear layer and an irregular enamel surface, which causes irregularities, thus increasing bond strength (2). Previous studies have already suggested that this laser can be used to create irregularities on the surface of ceramics from different types, and enhance the bond strength between these materials and resin cements (3, 4).

Nd: YAG laser modified the external surface of zirconia ceramics and yielded a smooth surface with irregular small Cirkonij-oksidna keramika ima vrhunska mehanička svojstva, uključujući visoku savojnu čvrstoću (1,0 – 1,2 GPa) i žilavost (7 – 8 MPa × m 0.5). Dodatno, razvoj nove tehnologije poput računalno potpomognutog dizajna/računalno potpomognote proizvodnje (CAD/CAM), omogućuje izradu svih keramičkih krunica (ili fiksne djelomične proteze) na ba- zi cirkonijeve oksida, što čini postupak praktičnijim. Cirkon- ska jezgra nadomjestka obložena je cirkonskom keramikom koja ima odgovarajući koeficijent termičke ekspanzije jezgri keramike. Kada jedan zub zahtijeva potpuno keramičku kru- niku (na bazi cirkonija), a drugi ljusku, kliničari se često suočavaju s izazovom pri odabiru materijala za restauraciju. Iako je poželjno na susjednim zubima korisiti istu obložnu keramiku, malo je dostupnih podataka o cirkonskoj obložnoj ke- ramici.

Litij-silikat ojačan cirkonijskim dioksidom (ZLS) temelji se na litij-metasilikatnoj (Li 2 SiO 3 ) staklokeramici i ojačan je s oko 10 % cirkonijeve dioksida (ZrO 2 ) 30) koji, nakon ko- načnoga procesa kristalizacije, potiče stvaranje sitnozrnate mikrostrukturo (Li 2 O–ZrO 2 –SiO 2 ). ZLS pripada novoj ge- neraciji materijala namijenjenih CAD/CAM uporabi koji kombinira izvrsna mehanička svojstva cirkonija i visoku estetiku staklokeramike. ZLS se, prema uputama proizvođača, može jetkati i cementirati adhezivnim sustavima, za razliku od cirkonskih nadomjestaka. Dokazano je da je otpornost na pucanje adhezivno cementirane, monolitne keramičke kruni- ce generirane CAD/CAM-om, znatno veća od one konvenci- onalno cementirane (1).

Jetkane i silanizirane, porculesne restauracije postale su prvi izbor u estetskoj rehabilitaciji prednjih zuba. Čvrstoća vezivanja kompozitne smole na adekvatno jetkan i silaniziran porculan premašuje kohezijsku čvrstoću porculana. Iako se vezanje na caklinu postiže samo jetkanjem površine radi postizanja mikromehaničke retencije, vezanje s porculanom postiže se mehanički jetkanjem porculana i kemijski uporabom silanskoga vezivnoga sredstva. Podatci iz literature po- dupiru silanizaciju porculana koja pruža pouzdaniju vezu od samo jetkanja fluorovodičnom kiselinom, iako se preporučuje kombinacija obaju postupaka.

Er: YAG laser djeluje termomehaničkom ablacijom ispa- ravajući vodu koja čini tkiva. Isparavanje uzrokuje ekspanziju praćenu mikroexplozijama, što izbacuje organske i anorg- ganske čestice iz tkiva, stvarajući izgled dentistinske površine s otvorenim tubulusima i bez zaostatnoga sloja te nepravilnu površinu cakline. Te razne nepravilnosti povećavaju čvrstoću veze (2). U dosadašnjim studijama autori su već sugerirali da se taj laser može koristiti za stvaranje nepravilnosti na površini keramike različitih vrsta te za povećanje čvrstoće veze izme- du tih materijala i smolastih cemenata (3, 4).

Nd: YAG laser je, kao posljedicu laserskoga zračenja, mo- dificira vanjsku površinu keramike i stvorio glatku površinu s nepravilnim, malim pukotinama. Taj nalaz u skladu je s dos- sadašnjim istraživanjima u kojima je izvješćeno o pukotinama na površinama cirkonija nakon laserskoga tretmana (5, 6).

Cilj ovog istraživanja bio je analizirati utjecaj različitih površinskih obrada litij-disilikatne keramike na čvrstoću vezivanja samoaderirajućega smolastoga cementa.
cracks due to laser irradiation. This finding is in line with the previous studies reporting cracks on zirconia surfaces after laser treatment (5, 6).

This study aimed to analyze the effect of different surface pretreatments of zirconium dioxide reinforced lithium disilicate ceramics on the shear bond strength with self-adhesive resin cement.

The null hypothesis was that the shear bond strength of composite self-etching cement to the surface of ZLS after surface treatment with Nd: YAG and Er: YAG laser would be the same as that of conventional preparation protocol (etching with hydrofluoric acid, silanization, sandblasting).

Materials and methods

Sample preparation

The material used in this research was lithium disilicate glass-ceramic reinforced with zirconium dioxide (Suprinty, Vita Zahnfabrik, Bad Sackingen, Germany). A total of 70 samples were made for the research purpose and cut into 18x12x2 size discs in the Isomet 1000 cutter. After cutting the discs, the material was crystallized according to the manufacturer’s instructions in the Programat P300 Furnace (Ivoclar Vivadent AG, Schaan, Liechtenstein).

After crystallization, the discs were prepared for polishing by being immersed in a silicone mold to be stationary when polished with 600 grit sandpaper lasting 1 minute for each cause. Polishing was performed at the Department of Materials of the Faculty of Mechanical Engineering and Naval Architecture, in order to make their surface uniform.

After polishing, the samples were embedded in acrylicate to completely fix their position when treating the surface.

Pretreatment protocols of lithium disilicate ceramic

After polishing, the samples were randomly divided into groups depending on the surface treatment method.

In the control group, after polishing with 600 grit sandpaper for a period of 1 minute, the samples were not treated at all.

Group 1 – Hydrofluoric acid

In the hydrofluoric acid group, the samples were treated with 9.5% hydrofluoric acid (Bisco Inc., Schaumburg, Illinois, USA) for a period of 90 seconds, whereupon the samples were washed with water and dried according to the manufacturer’s instructions.

Group 2 – Silanization

In the group subjected to the silanization process, the samples were treated with silane (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) for 60 seconds by rubbing silane with a brush on the surface of the sample, according to the manufacturer’s instructions.

Group 3 – Hydrofluoric acid + Silanization

In the group subjected to a combination of hydrofluoric acid and silane, the samples were treated with 9.5% hydrofluoric acid (Bisco Inc., Schaumburg, Illinois, USA) for 90 seconds, whereupon the samples were washed with water and dried according to the manufacturer’s instructions, and then treated with silane (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein).

Nulta hipoteza bila je da nema razlike u veznoj čvrstoći kompozitnoga samojetkajućega cementa na površinu ZLS-a nakon tretiranja površine laserima Nd:YAG i Er:YAG i konvencionalnog protokola pripreme (jetkanje fluorovodičnom kiselinom, silanizacija, pjeskarenje).

Materijal i metode

Pripremanje uzoraka

Materijal korišten u ovom istraživanju je litij disilikatna staklokeramika ojačana cirkonijevim dioksidom (Suprinty, Vita Zahnfabrik, Bad Sackingen, Njemačka). Ukupno je za potrebe istraživanja izrađeno 70 uzoraka koji su pripremljeni tako da su u rezalici Isomet 1000 rezani na diskove veličine 18 x 12 x 2. Nakon izrezivanja diskova materijal je kristaliziran prema utputama proizvođača za CEMADENT P300 (Ivoclar Vivadent AG, Schaan, Liechtenstein).

Nakon kristalizacije diskovi su pripremljeni za poliranje uranjenu u silikonski kalup kako bi bili nepomični pri poliranju brusnim papirima finoće 600 gura u trajanju od jedne minute po pojedinom uzroku. Poliranje je obavljeno u Zavodu za materijale Fakulteta za strojarstvo i brodogradnju kako bi se uniformirala njihova površina.

Nakon poliranja, uzorci su uloženi u akrylat da bi se potpuno fiksirala njihova pozicija pri tretiranju površine.

Protokoli obrađe litij-disilikatne keramike

Nakon poliranja uzorci su nasumično podijeljeni u skupine, ovisno o načinu tretiranja površine.

U kontrolnoj skupini uzorci nakon jednominutnoga poliranja 600-gritnim papirom nisu ni sa čime tretirani.

Skupina 1. – Fluorovodična kiselina

U skupini tretiranoj fluorovodičnom kiselinom uzorci su 90 sekunda tretirani 9,5-postotnom fluorovodičnom kiselinom (Bisco Inc., Schaumburg, Illinojs, SAD) nakon čega su isprani vodom i osušeni prema utputama proizvođača.

Skupina 2. – Silanizacija

U skupini podvrgnutoj procesu silanizacije uzorci su 60 sekunda tretirani silanom (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) na način da je silan utrljavan četkicom na površinu uzorka prema utputama proizvođača.

Skupina 3. – Fluorovodična kiselina + silanizacija

U skupini podvrgnutoj kombinaciji fluorovodične kiseline i silane uzorci su 90 sekunda tretirani 9,5-postotnom fluorovodičnom kiselinom (Bisco Inc., Schaumburg, Illinojs, SAD) nakon čega su isprani vodom i osušeni prema utputama proizvođača. Zatim su 60 sekunda tretirani silanom (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) tako da...
Schaan, Liechtenstein) in the duration of 60 seconds in a way that silane was rubbed with a brush on the surface of the sample, according to the manufacturer’s instructions.

**Group 4 – Sandblasting + silanization**

In the sandblasting group, the samples were sandblasted with 30 µm size Al₂O₃ particles (CoJet Sand, 3M ESPE, Neuss, Germany) at a pressure of 2.7 atm, and from sandblaster’s vertical distance of 1 cm from the sample in duration of 15 seconds. After sandblasting, the samples were washed under water, dried, and blown off to remove residual particles. The samples were then treated with silane (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) for 60 seconds. Silane was rubbed with a brush on the surface of the sample, according to the manufacturer’s instructions.

**Group 5 – Er:YAG irradiation + silanization**

In the group treated with Er:YAG laser, the samples were treated with a laser (LightWalker, Fotona, Slovenia) of the following parameters: pulse energy of 500 mJ with a power of 10 W and a frequency of 4 Hz for 20 seconds. After laser treatment, the samples were treated with silane (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) for a period of 60 seconds. Silane was rubbed with a brush on the surface of the sample, according to the manufacturer’s instructions.

**Group 6 – Nd:YAG irradiation + silanization**

The group treated with Nd: YAG laser was treated with a laser (LightWalker, Fotona, Slovenia) of the following parameters: 100 mJ pulse duration, frequency 20 Hz using a power of 1 W, after which the samples were treated with silane (Monobond, Ivoclar Vivadent AG, Schaan, Liechtenstein) for 60 seconds in a way that silane was rubbed with a brush on the surface of the sample, according to the manufacturer’s instructions.

**Shear bond strength test**

Before shear bond strength testing, it was necessary to make round shape composite disks (Filtek Bulk fill, 3M ESPE, St.Paul, Minnesota, USA) with a diameter of 3.5 mm, and cement them on the surface of the sample using composite cement (RelyX U200 Automix, 3M ESPE, Neuss, Germany).

After cementing the composite disk on the sample, the samples were subjected to a shear bond strength test at the School of Dental Medicine, University of Zagreb on a testing machine (type LRX with built-in Nexygen programme, Lloyd Instruments, Fareham, United Kingdom) at a test speed of 1 mm/ min. All tests were performed by the same person using force on the sample of 10 N with a “stress rate” of 1 MPa / s. Specimens were fixed in a testing jig. The load required to debond the specimen was recorded and expressed in MPa by dividing the load by the surface area of the bonded specimen, and the mean shear bond strength for each study group was calculated.

Fracture analysis of the sample surface in order to determine whether it was a cohesive, an adhesive, or a combined fracture were performed at the Department of Materials, Faculty of Mechanical Engineering and Naval Architecture, University of Zagreb using a stereomicroscope Mantis Elite-Cam HD (Vision Engineering Ltd, Woking, Great Britain), 20x optical magnification.
Surface roughness measurements were tested on the first, third and fifth samples within the same group, and on each of these samples the measurement was performed on six roughness profiles. A Gaussian filter was used for filtration, the limit value was set to $\lambda_c = 0.8$ mm, the probe radius $(r)$ of 5 µm, the grading length $(l_n)$ of 4.0 mm and the measuring force $(F)$ of 1.3 mN.

The effects of the laser irradiation on a surface of the zirconium reinforced lithium disilicate were examined by scanning electron microscopy (SEM). The SEM analysis was performed at the Department of Materials, Faculty of Mechanical Engineering and Naval Architecture, University of Zagreb. A Tescan Vega TS 5136 MM scanning microscope (TESCAN, Brno, Czech Republic) was used for topographic analysis. The analysis was performed by the same person at 300 x and 1000 x magnifications.

Statistical analysis

The ANOVA test and the Tukey test were used to compare the values of the bond strength characteristics between different types of materials. The Fisher's exact test was applied to compare the distribution of fracture types between different materials. The analysis was performed using the SAS statistical package on the Windows platform. All tests were performed with a significance level of $\alpha = 0.05$.

Results

For all tested protocols, the distribution did not deviate from the normal distribution (Table 1, $p > 0.05$).

Surface roughness analysis has shown that, for both sets of roughness data (Ra - arithmetic mean deviation of the profile and Rz - mean height of irregularities), the data distribution did not deviate significantly from the normal distribution ($p > 0.05$).

| Material • Materijal | N | Mean val. • Sr. vr. | Stand dev. • Sr. dev. | $W^{**}$ | $p^*$ |
|----------------------|---|---------------------|-----------------------|---------|-------|
| Control group • Kontrolna skupina | 5 | 2.51 | 3.11 | 0.83 | 0.14 |
| Acid • Kiselina | 7 | 11.45 | 5.15 | 0.83 | 0.13 |
| Silanization • Silanizacija | 7 | 12.92 | 4.23 | 0.89 | 0.29 |
| Acid + silanization • Kiselina + silanizacija | 7 | 8.92 | 4.09 | 0.95 | 0.74 |
| Sandblasting + silaniz. • Pjeskarenje + silanizacija | 7 | 11.93 | 6.18 | 0.98 | 0.97 |
| Nd:YAG + silanization • Nd:YAG + silanizacija | 8 | 15.91 | 7.28 | 0.92 | 0.44 |
| Er:YAG + silanization • Er:YAG + silanizacija | 6 | 6.78 | 2.64 | 0.87 | 0.23 |

$p^*$ - p-value for Shapiro-Wilk test • $p$ – vrijednost za Shapiro-Wilkov test

Rezultati

Za sve testirane protokole distribucija ne odstupa od normalne (tablica 1., $p > 0.05$).

Analiza hrapavosti pokazuje da za oba skupa podataka o hrapavosti (Ra – srednje aritmetičko odstupanje profila i Rz – srednja visina neravnina) distribucija podataka ne odstupa značajno od normalne ($p > 0.05$).

| Material • Materijal | Roughness (Ra) | Hrapavost (Ra) |
|----------------------|----------------|----------------|
| Control group • Kontrolna skupina | 127.8 | 90.2 |
| Acid • Kiselina | 75.2 | 106.8 |
| Silanization • Silanizacija | 106.8 | 282.1 |
| Acid + silanization • Kiselina + silanizacija | 282.1 | 100.7 |
| Sandblasting + silanization • Pjeskarenje + silanizacija | 1194.5 | 1194.5 |
Table 2. Različite vrijednosti površinske hrapanosti (Ra), ovisno o načinu predtretmana keramike.

Table 3. Usporedba snage vezivanja za različite protokole obrade površine keramike.

Table 4. Udio vrste loma nakon testiranih protokola za pripremu litij-disilikatne keramike.

Table 5. – Srednja vrijednost, standardna devijacija, medijan, prvi kvartil, treći kvartil, minimum i maksimum vrijednosti čvrstoće vezivanja između dentalne litij-disilikatne keramike ojačane cirkonijevim dioksidom i samoadherirajućeg kompozitnog cementa.

Tablica 2. – različite vrijednosti površinske hrapanosti (Ra), ovisno o načinu predtretmana keramike.
Tablica 3. – srednja vrijednost, standardna devijacija, medijan, prvi kvartil, treći kvartil, minimum i maksimum vrijednosti čvrstoće vezivanja između dentalne litij-disilikatne keramike ojačane cirkonijevim dioksidom i samoadherirajućeg kompozitnog cementa.
Tablica 4. – udio vrsta loma nakon ispitanih protokola za pripremu litij-disilikatne keramike ojačane cirkonijevim dioksidom.

Slika 1. – grafičko srednje vrijednosti vezne čvrstoće sa standardnom devijacijom nakon različitih protokola pripreme površine litij-disilikatne keramike.

Rezultati istraživanja pokazuju da postoji značajna razlika u veznoj čvrstoći samoadherirajućega cementa na dentalnu litij-disilikatnu keramiku ojačanu cirkonijevim dioksidom nakon različitih protokola pripreme (p < 0,05). Zabilježena je značajna veća snaga vezivanja nakon tretmana litij-disilikatne keramike ojačane cirkonijevim dioksidom postupkom silanizacije, pjeskarenjem i silanizacijom i laserskom Nd:YAG i silanizacijom u odnosu prema kontrolnoj skupini (u prosjeku 12,9 MPA, 11,9 MPA i 15,9 MPA u odnosu prema 2,5 MPA za kontrolnu skupinu).

Postoji statistički značajno veća vezna čvrstoća samoadherirajućega cementa nakon pretretmana litij-disilikatne keramike laserskom Nd:YAG i silanizacijom u usporedbi s laserskom Er:YAG i silanizacijom (u prosjeku 15,9 MPA u odnosu prema 6,8 MPA) (p < 0,05).

Distribucija vrste loma prema vrsti protokola prikazana je u tablici 4. U kontrolnoj skupini (slika 2.) i u skupini pje-
Figure 1  Shear bond strength of lithium disilicate ceramic to a self-adhesive cement after its different surface pretreatment
Slika 1. Snaga vezivanja samoadherirajućega cementa na litij-disilikatnu keramiku nakon različitih površinskih tretmana

Figure 2  Adhesive fracture in the control group
Slika 2. Adhezivna fraktura u kontrolnoj skupini

Figure 3  Adhesive fracture in the sandblasting + silanization group
Slika 3. Adhezivna fraktura u skupini pjeskarenje + silanizacija

Figure 4  Mixed fracture in the acid
Slika 4. Mješoviti lom u skupini tretiranoj kiselinom

Figure 5  Mixed fracture in silanization
Slika 5. Mješovita fraktura u silaniziranoj skupini

Figure 6  Mixed fracture in acid + silanization
Slika 6. Mješovita fraktura u skupini kiselina + silanizacija

Figure 7  Mixed fracture in Er: YAG + silanization group
Slika 7. Mješovita fraktura u skupini Er: YAG + silanizacija

Figure 8  Adhesive fracture in Nd: YAG
Slika 8. Adhezivna fraktura u skupini tretiranoj Nd: YAG laserom
tion group (Figure 3), while in the acid (Figure 4), silanization (Figure 5), acid + silanization (Figure 6), and Er: YAG + silanization group (Figure 7) mixed fracture dominates. In group Nd: YAG, the adhesive fracture also dominates (Figure 8), but with a share of 50%, while the share of mixed fracture is 37.5%.

Topographic architecture after surface treatment with different processing methods at magnifications of 300 and 1000 x was reviewed by SEM analysis.

Figure 9 SEM analysis after surface treatment with different processing methods skarenje + silanizacija (slika 3.) prevladava adhezivni lom, a u skupinama kiselina (slika 4.), silanizacija (slika 5.), kiselina + silanizacija (slika 6.) i Er:YAG + silanizacija (slika 7.) prevlađava mješoviti. U skupini Nd:YAG također prevladava adhezivni lom (slika 8.), ali s udjelom od 50 %, a udio mješovitoga loma je 37,5 %.

Topografska arhitektura nakon tretiranja površine različitim načinima obrade na povećanjima od 300 i 1000 puta pregledana je SEM analizom.

Slika 9. – SEM analiza nakon površinske obrade različitim metodama
Discussion

Despite continuous development and technological innovations, there is no material that is perfect on the market; therefore it is important to mention the shortcomings and complications in the therapy with these materials that occur due to fracture of the restoration, cement loosening, hypersensitivity, or abutment tooth carries. To ensure the durability and favorable biomechanics of such a ceramic appliance, its surface must be treated with chemical agents prior to cementing to the abutment tooth of the fixed prosthetic appliance. Technology development raises the question of the use of alternative systems that can affect the treatment and the roughness of the surface of ceramic material by acting on the shear bond strength of ceramics with dental cement. The use of dental laser is one of such alternative systems. Dental lasers are increasingly used in dental medicine, which places this area of research in the scientist's focus.

Although dental laser has been used for industrial purposes for a long period of time, its surface preparation is more recent. Laser preparation can change the surface microstructure of many materials and can be easily controlled (7, 8).

Previous research has shown that certain types of lasers, adjusted to certain parameters, can affect the surface roughness and characteristics of the material, thus directly affecting the shear bond strength system of ceramics. The energy released by laser can have beneficial effects on surface roughness by creating microcracks, thus forming an additional retention surface and improving the shear bond strength. However, laser-generated energy can also reduce the quality of the bond by dissolving the ceramic surface. In accordance with the newly created, smooth, dental surface of ceramic material, the laser reduces the shear bond strength, Ural and Kalyoncuoglu proved this in their research in 2012 by treating the surface of zirconium oxide ceramics with a CO2 laser. They observed that increasing the laser output power led to a decrease in the shear bond strength potential due to molten area formation on the ceramic surface (9).

A similar result was obtained by Hoosmand in 2015 using a Nd: Yag laser (shear bond strength potential weakening by creating molten areas on the ceramic surface), while Akin et al. showed that the Er: Yag laser had a beneficial effect on the shear bond strength creating microcracks and additional retention surfaces (10). It can be concluded that lasers and their influence on the shear bond strength when treating the dental ceramic's surface are unpredictable. The multitude of variables in the dental ceramics system, a large number of laser parametric combinations and the laser's surface length treatment provide research breadth, numerous opportunities for new observations, and innovativeness of the obtained results of individual research.

By standardizing the parameters for individual lasers, certain types of dental ceramics and variables responsible for shear bond strength, there will be a better understanding of bonding and processes that contribute to, or lead to bond failure, which is especially important to clinical work, thus ensuring quality and longevity of prosthetic therapy.

This study aimed to analyze the shear bond strength of self-adhering composite cement (RelyX U200 Automix, 3M, ESPE, Neuss, Njemačka) na površinu stakločarstvenih keramičkih materijala, te varijabli odgovornih za veznu čvrstoću. Uočili smo da povećanje izlazne snage lasera smanjuje potencijal vezne čvrstoće zbog stvaranja rastaljenih područja na površini keramike (9). Sljedeći rezultat dobio je i Hoosmand 2015, godine korišćenja Nd: Yag laserom (slabljene potencijal vezne čvrstoće zbog stvaranja rastaljenih područja na površini keramike), a Akin i suradnici u svojoj studiji pokazali su da Er: Yag laser povišava potencijal vezne čvrstoće na površini keramike, ali je važno spomenuti nedostatke i komplikacije u terapiji alternativnih sustava jest i dentalni laser koji se sve češće upotrebljava u dentalnoj medicini čime i to područje istraživanja dolazi u fokus znanstvenika.

Rasprava

Unatoč kontinuiranom razvoju i tehnološkim inovacijama, na tržištu još nema idealnoga građivina materijala tako da je važno spomenuti nedostatke i komplikacije u terapiji tim materijalima koje nastaju zbog puknula, popuštanja cementa, preosjetljivosti ili karijesa uporišnog zuba. Kako bi se osigurala trajnost i povoljna biomehanika taka keramičkoga rada, njegova se površina mora tretirati kimjskim agensima prije nego li bude cementiran na sub nosač fiksnooprotetičkog rada. Razvojem tehnologije postavlja se pitanje upotrebe alternativnih sustava koji mogu utjecati na obradu i hravost površine keramike djelujući na veznu čvrstoću keramike s dentalnim cementom. Jedan od takvih alternativnih sustava jest i dentalni laser koji se sve češće upotrebljava u dentalnoj medicini čime i to područje istraživanja dolazi u fokus znanstvenika.

Iako se laser već dulje primjenjuje u industrijske svrhe, priprema površine laserom novijeg je datum. Riječ je o postupku kojim se može mijenjati mikrostruktura površina mnogih materijala i koji je moguće jednostavno kontrolirati (7, 8).

Dosadašnja istraživanja pokazala su da pojedine vrste lasera, podešene na određene parametre, mogu utjecati na površinsku hravost i svojstva materijala i tako izravno utjecati na veznu čvrstoću keramičkoga sustava. Energija koju laser oslobađa može korisno utjecati na površinsku hravost stvarajući mikropukotine čime nastaje dodatna retencija površina i boljša se vezna čvrstoća. No laserom stvorena energija može i smanjiti kvalitetu veze djelujući tako da rastali površinu keramike i, ukladno novonastaloj glatkoj površini keramičkoga materijala, smanji veznu čvrstoću. To su 2012. godine dokazali Ural i Kalyoncuoglu u svojem istraživačkom radu tretirajući površinu cirkonij-oksidske keramike CO2 laserom. Uočili su da povećanje izlazne snage lasera smanjuje potencijal vezne čvrstoće zbog stvaranja rastaljenih područja na površini keramike (9).

Sljedeći rezultat dobio je i Hoosmand 2015, godine korišćenja Nd: Yag laserom (slabljene potencijal vezne čvrstoće zbog stvaranja rastaljenih područja na površini keramike), a Akin i suradnici u svojoj studiji pokazali su da Er: Yag laser povišava potencijal vezne čvrstoće na površini keramike, ali je važno spomenuti nedostatke i komplikacije u terapiji alternativnih sustava jest i dentalni laser koji se sve češće upotrebljava u dentalnoj medicini čime i to područje istraživanja dolazi u fokus znanstvenika.
ESPE, Neuss, Germany) to the surface of glass ceramics reinforced with zirconium oxide (Suprinity, Vita Zahnfabrik, Bad Sackingen, Germany) after different surface pretreatments. The aim of the survey was also to examine the effect of laser radiation (Er:YAG, Nd:YAG) on the surface (qualitative micromorphological analysis of the ceramics surface samples using SEM, microchemical X-ray spectroscopy using EDX and X-ray diffraction analysis, XRD), surface roughness (profilometry) and samples shear strength with fracture analysis and to compare with conventional surface preparation protocols (sandblasting, etching with hydrofluoric acid, silanization).

After the process of controlled glass crystallization, the introduction and invention of glass-ceramics, from the first Nycor glass through leucite (IPS Empress) and ceramics with mica crystals (Dicor ceramics), then lithium disilicate (IPS Empress 2 and E-max ceramics) and finally hybrid, lithium disilicate glass-ceramics reinforced with zirconium dioxide have occurred in a relatively short period. Leucite glass-ceramics were used to make individual crowns in the anterior (layering technique) or posterior (staining technique) segment of dentition and onlay, inlay, and overlay. It was quickly noticed that such a narrow indication area, which characterized both first generations of glass-ceramics, was not profitable. Therefore, various attempts were made to strengthen glass-ceramics with the intention of using it for greater constructions. The crystal structure, quantity, arrangement, and crystals size were changed; secondary phases were introduced until the final reinforcement with zirconium oxide. Such a combination resulted in very desirable building material in fixed prosthetic therapy that combines good properties of glass-ceramics (the possibility of achieving excellent esthetics) and zirconium oxide (outstanding mechanical properties). Ensuring a quality connection between the restoration and the abutment tooth can be observed through two aspects: prosthetic appliance surface preparation made of ceramic material and abutment tooth surface preparation. The inner surface of ceramics must be conditioned to ensure optimal micro-mechanical retention by penetrating the composite into the ceramic micro-roughness surface; this procedure increases the cement mechanical retention by increasing the contact surface with the tooth structure through the micro-porosity formation. Roughness formation and promotion of micro-mechanical retention, different ways of surface treatment in contact such as abrasive treatment, sandblasting, and acid etching have been well explained in the literature (11, 12). These procedures were tested in in vitro studies. In vitro studies and the results obtained by such studies have their limitations; therefore it is necessary to take them with reserve. As much as in vitro research can simulate conditions in the oral cavity, it is still difficult to obtain identical conditions since the oral cavity is a specific and complex medium from both a mechanical and a corrosive point of view. However, in vitro studies are easier to conduct, and they are also cheaper and faster. Their results can be used as a guide to help interpret with considerable certainty a wide range of developments in the oral cavity. This attitude is widely accepted in the scientific community.
Tian has stated that the most commonly used technique for preparing the surface of a glass-ceramic restoration before cementation is treatment with hydrofluoric acid and silanization (13). During this procedure, the surface was partially dissolved and the crystals were partially stripped, leading to a rough ceramic surface formation that provided micromechanical retention with the composite cement. An additional roughness increase enlarges the surface energy and interaction between the binder and silane, which promoted the chemical-mechanical adhesion between the ceramic / silane/cement surface (14). While hydrofluoric acid increases the shear bond strength between cement and ceramics, the acid simultaneously reduces the material mechanical resistance depending on the acid concentration and the conditioning time. These factors can also change the shear bond strength between composite cement and glass-ceramics (15).

Cement should ensure good replacement retention and quality edge fitting, but its contribution to modern building materials application is certainly in providing better optical properties of prosthetic appliance. The first types of cements were aqueous suspensions, such as zinc phosphate and glass-ionomer cement. By introducing composite cement, properties such as solubility and adhesion have been improved by enabling a minimally invasive abutment tooth preparation form. The esthetic property of composite cement is of great importance in modern esthetic prosthodontics; therefore, composite cement is becoming more and more common in dental medicine. It consists of three parts: an organic resin matrix consisting of bis-GMA or urethane-dimethacrylates (UDMA), inorganic filler particles, and a binder (bonding intermediate layer). They are characterized by high compressive and tensile strength, the ability to achieve a micromechanical bond with enamel, dentin, dental alloys, and ceramics. Composite cement together with an adhesive bonding system makes up adhesive cementation. The bond achieved by adhesive cementation can be mechanical, micromechanical, and chemical at the molecular level.

The results of this study showed that the best shear bond strength was achieved after surface treatment with Nd:Yag laser in combination with silanization, while the application of Er:Yag laser has achieved lower values of shear bond strength compared to conventional surface preparation methods (sandblasting, etching, silanization), which makes the second null hypothesis (no difference in shear bond strength between laser-treated surfaces and conventional surface preparation methods) rejected, while the second working hypothesis (shear bond strength is higher after laser treatment) is partially accepted. The largest contact area was obtained in samples treated with Nd:Yag laser.

Scanning electron microscopy analysis of fractured surfaces showed the adhesive type of fractures (largest in samples sandblasting + silanization, absent in samples treated with acid, silanization, and acid + silanization), cohesive type of fracture (same within samples treated with acid, sandblasting + silanization, and Nd: laser + silanization, while in other samples this type of fracture did not occur) and mixed type of fracture (highest in samples treated with silanization and acid nja tretiranje florovodičnom kiselinom i silanizacijom (13). U tom postupku površina je djelomično otopljenina i kristali su dijelom ogoljeni, što je poticalo stvaranje hrapave površine na keramiku koja je osiguravala mikromehaničku retenciju s kompozitnim cementom. Dodatnim povećanjem hrapavosti raste površinska energija i interakcija između veznoga sredstva i silana, što je promoviralo kemijsko-mehaničku adheziju između keramike/silana/cementne površine (14). Dok florovodična kiselina povećava veznu čvrstoću između cementa i keramike, kiselina istodobno smanjuje mehaničku otpornost materijala, ovisno o koncentraciji kiseline i duljinii kondicijoniranja. Ti čimbenici mogu također mijenjati veznu čvrstoću između kompozitnog cementa i staklokeramike (15). Cement bi trebao osigurati dobru retenciju nadomjesta i kvalitetno rubno prilijeganje, ali njegov doprinos u primjeni suvremenih gradivnih materijala svakako je i u osiguranju boljih optičkih svojstava protetičkoga rada. Prvi cementi bili su vodene suspenzije, poput cink-fosfatnih i stakloionomernih cemena. Uvođenjem kompozitnih cemena, svojstva poput rastvorljivosti i adhezije poboljšana su i omogućuju minimalno invazivan preparacijski oblik uporišnoga zuba. Estetsko svojstvo kompozitnih cemena vrlo je važno u suvremenom estetskom pretreti i zato taj materijal postaje sve za-stupljeniji u dentalnoj medicini. Tvoe ga tri dijela: organska smolasta matrica koju čine bis-GMA ili uretan-dimetakrilata (UDMA), anorganske čestice punile te vezujuće sredstvo (spojni medusloj). Karakterizira ih velika tlačna i vlačna čvrstoća, moguće postizanje mikromehaničke veze s caklinom, dentinom, dentalnim legurama i keramikama. Kompozitni cement, zajedno s adhezijskim sustavom veze, čini adhezijsko cementiranje. Veza koju je moguće postići adhezijskim cementiranjem jest mehanička, mikromehanička i kemijska na molekularnoj razini.

Rezultati ovog istraživanja pokazuju da je najbolja vezna čvrstoća postignuta nakon tretiranja površine Nd:Yag laserom u kombinaciji sa silanizacijom, a da primjena Er:Yag lasera ostvaruje niže vrijednosti vezne čvrstoće u odnosu prema konvencionalnim načinima pripreme površine (pjeskarenje, jetkanje, silanizacija), čime se odbacuje druga nulta hipoteza (nema razlike u veznoj čvrstoći između površina obrađenih laserom i konvencionalnih načina obrade površine), a djelomično se prihvaća druga radna hipoteza (vezna čvrstoća veća je nakon tretmana laserom). Istatkno je da je u ovom istraživanju dobivena najveća kontaktna površina na uzorcima tretiranima Nd:Yag laserom. Analiza pretražne elektronske mikroskopije fruktuiranih površina upućuje na to da se radi o adhezivnom lomu (najveći kod uzoraka pjeskarenje + silanizacija, nema ga na uzorcima tretiranima kiselinom, silanizacijom i kiselinom + silanizacijom) i kohezivnom tipu loma (jednak kod uzoraka tretiranih kiselinom, pjeskarenjem + silanizacijom te Nd:Yag laserom + silanizacijom, a u ostalim uzorcima nije se dogodila ta vrsta loma) i mješovitom tipu loma (najveći na uzorcima tretiranim silanizacijom te kiselinom i silanizacijom, a u kontrolnoj skupini nema te vrste loma).

Na kvalitetu veze, odnosno na veznu čvrstoću staklokeramike i kompozitnog veznoga sredstva, utječe niz čimbenika. Svi imaju jedan imperativ – postići kvalitetnu vezu koja osi-
The quality of the bond, i.e. the shear bond strength of the glass-ceramic and composite bonding agent, is influenced by numerous factors. The imperative is known to everyone - to achieve a quality bond that ensures the durability of prosthetic appliance. Different methods of glass-ceramic surface treatment before cementation have been described in the literature and applied in clinical work, all of them aimed to achieve the best possible bond between the restoration and the abutment tooth. The most common way to test the bond strength is the shear test. This test shows the occurrence of cohesive fracture within a material more often than at the junction of two materials. The result is explained by the strong stress accumulation during testing which can lead to test results misinterpretation. Consequently, it is important to eliminate uneven stress within the adhesive zone. Some authors have used very small test areas of only 1 mm² to create a uniformly transmitted stress to the joint surface (16, 17, 18). In this way, detection of the weakest points of the procedure is enabled. In the machine production process of restoration, the impact of this procedure on the cutting surfaces should be taken into consideration. The milled sample's SEM analysis shows visible crystals on the cutting surface, which improve micromechanical retention and increase the bonding surface with composite cement. These results were confirmed by this study. This interpretation confirms the hypothesis that it may be possible to establish a quality bond with glass-ceramics chains without etching with hydrofluoric acid (16). Pollington has claimed that SEM analysis of machine processed lithium-disilicate glass-ceramics surface revealed the presence of microporosity which may be of significant importance in achieving a micromechanical bond between the restoration and the abutment tooth surface. He pointed out that this type of complete ceramic must be subjected to additional surface treatment procedures to provide sufficient micro retention for quality bond achievement (19). If a cohesive fracture of the binder dominates, it occurs due to microcracks inside the cement rather than the intermediate joint itself.

Silane use as a bond promoter between the ceramics and the binder is a well-known fact (20). The bond with the ceramics is achieved through a condensation reaction between silanol groups (Si-OH) on the ceramic surface and hydrolyzed silane silanol groups, which forms a siloxane bond (Si-O-Si) and produces a water molecule as a by-product (21). The presence of a glassy phase in ceramics promotes forming of a better siloxane bond. The silanol groups then react by forming a siloxane network with silicon on the surface (22). An important factor in the chemical bond between the two materials is silicon from glass. This finding by Pollington is consistent with an earlier claim that etching is not necessary (19).

Mean roughness value and SEM analysis showed an irregular surface with pronounced porosity and undermined sites. This surface is visibly weakened by the action of hydrofluoric acid. This is also confirmed by other authors (23).

Glass-ceramics sandblasting leads to extreme destruction of glass and crystals. The crystals obliterate dentinal tubules and produce a water molecule as a by-product (21). The presence of a glassy phase in ceramics promotes forming of a better siloxane bond. The silanol groups then react by forming a siloxane network with silicon on the surface (22). An important factor in the chemical bond between the two materials is silicon from glass. This finding by Pollington is consistent with an earlier claim that etching is not necessary (19).

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and lead to impossibility of ensuring a quality connection. Another reason for poor bonding is the contamination and deposition of alumina particles on the ceramic surface. Us-
tun et al. have claimed that the surface treatment affects sur-
face roughness and stated that sandblasting achieves signifi-
cantly higher values of bond strength compared to the surface
treated with Erbi laser (24). The abovementioned facts have
been confirmed by this research. The abovementioned au-
thors prefer sandblasting over the application of Er:Yag la-
sers. Bond quality tests between ceramics and composite ce-
cement can be carried out by tests such as aging corrosion and
alike (25). Water storage leads to gradual water absorption
within the composite, which can lead to hydrolytic degrada-
tion and consequently to bond weakening between the ce-
ramic and the composite cement; silane bond hydrolysis is
likely to occur (26, 27).

Numerous authors concur that the optimum bond be-
tween composite cement and glass-ceramics varies for dif-
ferent ceramic systems. It cannot be expected that a single
procedure will be universal for all-ceramic materials. This re-
alization is crucial since new ceramic materials of different
compositions and microstructures will appear on the market.

All the above-named procedures require micromechanical
locking on the joint surface and a chemical bond be-
tween the joint surfaces; therefore it is necessary to intervene
in some way in the surface structure of the material and/or
teeth. Research on non-aggressive procedures is becoming
more pronounced by modifying the surface texture and ma-
terial chemical properties on the surface, which makes the
surface more activated, i.e. a functional surface is created
(28). The acid dissolves the ceramic surface by dissolving
the glass phase. It leads to the irregular formation on the surface
and increases the contact surface (29). Adhesion between ce-
ramics and composite cement is the result of physicochemical
interaction in the interface between composites (adhesives)
and ceramics (substrates). The surface treatment and its to-
pography will contribute to physical interactions of adhesion.
Modifications in topography surface achieved by sandblast-
ing will result in changes in substrate moisture, which corre-
lates with surface energy and adhesive potential (30). Rough
surface increases mechanical retention by enabling adhesive
interlocking (locking) in surface irregularities (31). Unfortu-
nately, several studies have demonstrated the possibility of
ceramic surface weakening after etching, thus leading to fast-
er fracture of the restoration (32). Although the application
of dental laser for surface preparation before cementation is
not exempt from difficulties, it nevertheless promises. Some
tests of CW CO2 lasers impact with 10.6 µm on lithium di-
silicate (33) and CAD-CAM ceramic (25) confirm the pres-
ence of micro-cracks and surface dissolution, as a result of the
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Nd: YAP
laser irradiation can be correlated with high thermal values leading to extreme physical stress and additional ceramic surface hardening (4, 35). Er: YAG lasers can be used to treat the surface of alumina ceramics, but their result is much weaker than the one achieved by etching. The most probable explanation for this is that energy generated by the Er: YAG laser cannot be absorbed as well as in this type of ceramic, and it does not create a sufficient micro-mechanical retention (36). According to this study, some authors recommended the use of very high energy (500 mJ) to achieve a satisfactory retention (37). The most recent types of ultra-short pulsed lasers may achieve better results (38).

Despite the results of numerous studies, the application of lasers is still an alternative method in surface preparation in order to achieve a better connection between two surfaces in contact. Lasers modify the material surface in a relatively light and simple way. In ZrO2 ceramics, the laser does not form the desired roughness because these irregularities are very shallow and do not provide micromechanical retention, meaning there is no increase in bond strength. Compared to tribochemical processing, the laser is less efficient. During laser surface treatment, created clusters can stick to the melted ceramic surface, leading to quality bond impairment (39).

Er: Yag is the most commonly used laser in clinical practice. The wavelength is approximately 2940 nm. These types of lasers make the surface irregular, which increases the micromechanical retention of the ceramic material. Lasers with longer wavelengths can damage the surface by creating cracks, thus weakening the bond (40). The findings of previously mentioned studies are contradictory and are not in line with findings of the present survey. Numerous factors such as ceramic moisture, surface roughness, binder, and chemical composition can affect the composite cement quality and stability and its bond to the ceramic surface (2). Gomes et al. thermocycled zirconium oxide ceramics samples cemented with composite cement and concluded that shear bond strength is affected by surface treatment, aging, and cement type (38). On the contrary, Subasi (41) believes that cement type has the greatest impact on shear bond strength, while Oyagüe favors pretreatment of the joint surface (42). The SEM analysis shows that the once treated surface always remains rough, and has uniform round micro retentions and shallow holes, but without microcracks. Silane contains silicon-bonded to reactive organic radicals that chemically bind to composite molecules forming siloxanes with silicon-coated surfaces. This improves the ceramic humidity (creating better contact and composite infiltration into the ceramic irregularity), protecting it from moisture and creating an acidic environment that can support the bonding mechanisms (43, 44).

Zirconia ceramics does not contain water, which can affect absorption of laser energy. Therefore, some studies did not find a significant increase of the micromechanical bond between cement and ceramics (45). However, Spohr et al. (46) and Usuzmet al. (47) concluded that Nd:YAG laser irradiation increased both, the surface roughness and shear bond strength. Our results also revealed an increase in surface roughness and bond strength due to Nd:YAG laser irradiation.
Conclusions

Under the limitations of this study, the Nd:YAG irradiation with silanization could be used as pretreatment for providing greater shear bond strength of self-adhesive resin cement to zirconium reinforced lithium disilicate. The pretreatment with ER:YAG irradiation did not increase the bond strength compared to the conventional pretreatment protocol.

Conflict of interest

The authors declared no conflict of interest.

Author’s contribution: A.C., D.K., I.B. - made a research plan, preparation of samples, and they performed laboratory testing; A.C., D.K., I.B., D.N.V., J.K., B.B. - searched the literature, analyzed the obtained results and participated in manuscript writing.

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Zaključak

Uzimajući u obzir ograničenja ovog istraživanja, Nd:Yag lasersko zračenje u kombinaciji sa silanizacijom moglo bi se koristiti kao predtretman u svrhu osiguravanja bolje čvrstoće vezivanja samoadherirajućega smolastoga cementa i litij-disilikatne keramike ojačane cirkonijevim dioksidom. Predtretman Er: YAG laserom nije povećao čvrstoću vezivanja u usporedbi s konvencionalnim protokolom obrade.

Sukob interesa

Autori nisu bili u sukobu interesa.

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