Ascorbyl palmitate/D-α-tocopheryl polyethylene glycol 1000 succinate monoester mixed micelles for prolonged circulation and targeted delivery of compound K for antilung cancer therapy in vitro and in vivo

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Abstract: The roles of ginsenoside compound K (CK) in inhibiting tumor have been widely recognized in recent years. However, low water solubility and significant P-gp efflux have restricted its application. In this study, CK ascorbyl palmitate (AP)/D-α-tocopheryl polyethylene glycol 1000 succinate monoester (TPGS) mixed micelles were prepared as a delivery system to increase the absorption and targeted antitumor effect of CK. Consequently, the solubility of CK increased from 35.2±4.3 to 1,463.2±153.3 µg/mL. Furthermore, in an in vitro A549 cell model, CK AP/TPGS mixed micelles significantly inhibited cell growth, induced G0/G1 phase cell cycle arrest, induced cell apoptosis, and inhibited cell migration compared to free CK, all indicating that the developed micellar delivery system could increase the antitumor effect of CK in vitro. Both in vitro cellular fluorescence uptake and in vivo near-infrared imaging studies indicated that AP/TPGS mixed micelles can promote cellular uptake and enhance tumor targeting. Moreover, studies in the A549 lung cancer xenograft mouse model showed that CK AP/TPGS mixed micelles are an efficient tumor-targeted drug delivery system with an effective antitumor effect. Western blot analysis further confirmed that the marked antitumor effect in vivo could likely be due to apoptosis promotion and P-gp efflux inhibition. Therefore, these findings suggest that the AP/TPGS mixed micellar delivery system could be an efficient delivery strategy for enhanced tumor targeting and antitumor effects.

Keywords: ginsenoside CK, ascorbyl palmitate, TPGS, mixed micelles, anti-tumor therapy

Introduction
Approximately 1.8 million new lung cancer cases and 1.6 million lung cancer-related deaths were reported in 2012, accounting for the highest reported incidence of mortality.1 In an attempt to decrease the high mortality rate of lung cancer, more attention needs to be focused on finding alternative treatment methods.

Ginsenosides, the major active compounds of ginseng, have been widely used for different applications, especially for cancer.2,3 Compound K (CK) is one of the major metabolites of ginsenosides that exhibits maximal antitumor effect.4,5 However, its low water solubility, poor permeability, and significant P-gp efflux restrict its application.6,7 Therefore, the goal of this study was to increase the solubility, targeted efficacy, and antitumor effect via formation of mixed micelles.
Binary mixed micelles of surfactants in aqueous solutions have wide applications. Lesser amounts of substance are used in the industrial application of such mixtures of surfactants than individual surfactants. The interactions between different units of mixed micelles could make it more stable. In addition, the application of binary mixture of surfactants, especially for obtaining micellar solutions, by changing the molar fraction of the surfactants in their binary mixture, can lead to an increased solubility capacity of the micellar system. \( \text{D-\textalpha-Tocopheryl polyethylene glycol 1000 succinate monoester (TPGS)} \) is a PEGylated vitamin E that has great advantages in enhancing the solubility and inhibiting P-gp efflux. In addition, after micelle formation, it can escape recognition and elimination in vivo and has a prolonged circulation. It is also generally regarded as a safe listed oral supplement, which has been approved by the US Food and Drug Administration as a safe pharmaceutical adjuvant used in drug formulation, and has been investigated for oral and parenteral administration in antineoplastic therapy. \( \text{Ascorbyl palmitate (AP), an amphiphilic derivative of ascorbic acid that has antioxidant activity, can also self-aggregate and form micellar structures in aqueous media} \). \( \text{Ascorbate has been shown to increase the effectiveness of various anticancer treatments} \). Mixed micelles composed of TPGS and AP are nanosized colloidal particles with a hydrophobic core and a hydrophilic corona. The hydrophobic segment forms the core of the micelles that solubilize the hydrophobic drug molecules, and the hydrophilic segment forms the corona that provides compatibility of the micelles in the aqueous environment. The hydrophobic core accommodates various hydrophobic molecules, such as therapeutics and imaging agents, thus improving the solubility and stability in the biological system. The hydrophilic corona shields the core and protects the loaded drugs from interactions with the blood components. The biocompatible polymeric corona causes reduced recognition of the micelles by reticuloendothelial systems, thus providing prolonged circulation of the loaded component in the blood stream. The nanoranged size along with the prolonged circulatory property allows mixed micelles to eventually accumulate in any compromised tissue vasculature sites, eg, tumor via a passive targeting phenomenon commonly referred to as enhanced permeability and retention effect.

Therefore, the overarching aim of the current study was to design a novel AP/TPGS mixed micellar system and investigate its potential targeted therapeutic effect in treating lung cancer in vitro and in vivo. The AP/TPGS mixed micelles of CK could enhance the water solubility and permeability of CK, prolong its retention time, and promote its accumulation in tumor tissues. It could be a potential alternative for effective and targeted tumor therapy.

**Materials and methods**

**Preparation and characterization of CK mixed micelles**

CK-loaded AP/TPGS mixed micelles were prepared as follows: CK, TPGS, and AP were dissolved in ethanol to form a clear solution. Then, the organic solvent was evaporated under vacuum at 40°C to form a thin film. The thin film was hydrated by deionized water for 30 min at 40°C to form the mixed micelles. \( 1,1'-\text{dioctadecyl-3,3,3', 3'-tetramethylindotricarbocyanine iodide (DiR)} \) mixed micelles and coumarin-6 mixed micelles were also prepared by the abovementioned method with the substitution of DiR and coumarin-6 for CK, respectively.

**Particle size, polydispersity, and morphology**

Size, zeta potential, and polydispersity of the CK mixed micelles were determined using Malvern Zetasizer Instruments (Nano ZS; Malvern Instruments, Malvern, UK). A total of 2 mL of mixed micelles was taken in a polystyrene disposable cuvette and exposed to laser light diffraction at an angle of 90° to determine size and polydispersity. A total of 1 mL of mixed micelles was placed in the electrophoretic cell of the Malvern Zetasizer Nano ZS and the average surface charge was determined. To verify the reproducibility of results, the experiments were performed in triplicate.

Morphology of the mixed micellar formulations was observed using a transmission electron microscope (JEM 100CX, JEOL, Tokyo, Japan).

**The drug loading content (LC) of mixed micelles**

The drug LC was measured by a high-performance liquid chromatography (HPLC) method. The mixed micelles were spun down at 13,000xg for 15 min; 200 μL of the supernatants was diluted in 800 μL of methanol and analyzed for CK.

The drug LC and encapsulation efficiency (EE) of CK mixed micelles were calculated using the following formulae:

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\text{LC } (\%) = \frac{\text{Mass of CK encapsulated in micelles}}{\text{Mass of mixed micelles}} \times 100% \\
\text{EE } (\%) = \frac{\text{Mass of CK in micelles}}{\text{Mass of feeding CK}} \times 100%.
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Solubility measurements

Classical approaches for measuring solubility are based on the saturation shake-flask method. Excess amounts of CK were placed into 5 mL vials containing aqueous solutions. The vials were sealed and placed into a constant temperature bath (37°C) and shaken for 24 h, until equilibrium was evident. After centrifugation of the incubated suspensions at 37°C and 15,000 rpm for 15 min, the concentrations of CK in the supernatant solutions were determined by an HPLC procedure, and the concentration of CK in the micellar system was determined after a 100 times dilution with methanol and then analyzed for CK.

Stability of CK mixed micelles

A total of 100 µL of CK mixed micelles was diluted with phosphate buffered saline (PBS) buffer (pH 7.4) to 1 mL and incubated at 37°C for 7 days. The variance of particle size and solubility were measured once a day.

In vitro drug release

The in vitro drug release of the CK mixed micelles was evaluated by dialysis bag diffusion. The CK mixed micelles at a volume equivalent to 50 mg of free CK were added to a dialysis bag and immersed into 50 mL of PBS containing 0.2% w/v Tween 80 with continuous shaking at 100 rpm at 37°C. Isopycnic fresh medium was replaced after withdrawal from the receptor compartment. The samples were filtered through a 0.45 µm syringe filter before being transferred into an HPLC vial.

In vitro cellular uptake

Following incubation of A549 cells (purchased from Nanjing KeyGen Biotech Co. Ltd, Nanjing, People’s Republic of China) in glass-bottomed dishes containing culture medium at 37°C for 24 h, cell culture media containing coumarin-6 solution and coumarin-6-loaded mixed micelles were added and incubated for 4 h at 37°C. The A549 cells were washed with ice-cold PBS twice and fixed with 95% ethanol for 20 min. Then, the cells were fixed with paraformaldehyde and stained with 4′,6-diamidino-2-phenylindole (DAPI) for 15 min. The fluorescent images of the cells were observed under a fluorescence microscope (IX71; Olympus Corp, Tokyo, Japan) and a Leica confocal laser scanning microscope (CLSM; TCS SP5; Leica, Heidelberg, Germany).

Cell viability assay

Cells were seeded in 96-well plates and treated with CK or CK mixed micelles. The different concentrations of CK or CK mixed micelles were 5, 10, 20, 40, and 80 µg/mL. The untreated cells were used as control for this study. After incubation for 24 h, the cells were stained with 3-(4,5-dimethyl-2-thiazoly)-2,5-diphenyl-2-H-tetrazolium bromide for 4 h. The blue crystals in cells were dissolved with dimethyl sulfoxide. The absorbance intensity was then measured using a microplate reader at an absorbance wavelength of 570 nm after subtracting the background absorbance at 660 nm.

TUNEL analysis

DNA fragmentation was detected in situ by TUNEL staining. Briefly, after being treated with CK or CK mixed micelles, A549 cells were permeabilized by Tris-HCl and ethylenediaminetetraacetic acid (EDTA) for 10 min. The cells were then washed, fixed, and labeled with TUNEL reaction mixture at 37°C for 60 min in the dark. The nuclei of apoptotic cells were stained brown. However, the nuclei of normal cells were purple. The morphology of cells was recorded by photography.

Cell apoptosis

A549 cells were incubated with CK or CK mixed micelles at a CK concentration of 10 µg/mL for 24 h. After washing twice with ice-cold PBS, the cells were harvested with trypsin–EDTA and resuspended at 1×10⁶ cells/mL. Cell suspensions (100 µL) were kept in the dark and stained simultaneously with fluorescein isothiocyanate-annexin V and propidium iodide (PI) for 10 min at 37°C, and then apoptosis was analyzed by flow cytometry.

Cell cycle analysis

A549 cells were seeded into 6-well plates and cultured. After exposure to CK or CK mixed micelles at 10 µg/mL of CK for 24 h, A549 cells were harvested with trypsin–EDTA. After washing twice with ice-cold PBS, the cells were fixed with 70% ethanol and stored at 4°C for 12 h. Before analyzing the DNA content, samples were suspended in 1.0 mL hypotonic PI solution, and incubated in the dark for 30 min prior to flow cytometric analysis.

Cell migration assay

A549 cells were seeded onto a 12-well plate to obtain a cell monolayer. A 200 µL pipette tip was then used to produce a vertical wound. Wounded cells were removed by gently washing twice with PBS. Then, free CK or CK mixed micelles in serum-free medium was added to the cells, which were incubated for an additional 24 h. The cells were photographed, and the width of the wound was evaluated using a microscope.
Animals
Nude mice (20±2 g body weight) were purchased from SLEK Lab Animal Center of Shanghai (Shanghai, People’s Republic of China). All animal experiments were performed in accordance with institutional principles of care and use of laboratory animals (revised according to the national standard) and were approved by the experimental animal administrative committee of The First Hospital of Suqian. We confirm that ethical and legal approval was obtained prior to the commencement of the study.

Targeted effect of DiR-loaded mixed micelles in vivo
A549 cell suspension was inoculated into nude mice via a hypodermic injection, and the mice were divided into two groups (n=3) when the tumor volume reached ~150 mm³. The mice were then administered DiR or DiR mixed micelles via tail vein injections for imaging study, anesthetized via isoflurane, and evaluated at 1, 2, 4, 8, and 24 h using the IVIS 200 imaging system (PerkinElmer, Hopkinton, MA, USA) at an excitation/emission wavelength of 625/700 nm, respectively. The exposure time was 30 s per image. After in vivo imaging, the major tissues were obtained to determine the associated fluorescence intensities for ex vivo imaging.

Antitumor efficacy in lung cancer xenografts
Nude mice were used for investigating the antitumor efficacy in vivo when tumor volume reached 50 mm³. The mice were randomly divided into three treatment groups (five in each group). Then, saline, CK (30 mg/kg), or CK mixed micelles (30 mg/kg) were administered via tail vein injections every 3 days until the 12th day. The tumor volumes and body weight were recorded every 3 days until the 15th day. Tumor volumes were calculated as length × width²/2 (mm³). At the end of the experiment, the tumor, liver, and kidney were obtained for pathological study by hematoxylin and eosin (H&E).

Western blot analysis
The tumor cell lysates were separated by sodium dodecyl sulfate polyacrylamide gel electrophoresis (SDS-PAGE) and transferred onto polyvinylidene difluoride (PVDF) membranes. The membranes were incubated with specific primary antibodies at 4°C for 12 h and visualized using a Western blotting detection system. Caspase 3, caspase 8, caspase 9, P-gp, Bax, and Bcl-2 antibodies were obtained from Santa Cruz Biotechnology, Inc. (Santa Cruz, CA, USA). The results of Western blot were analyzed by gray level of chemiluminescence.

Statistical analysis
Data are presented as mean ± standard deviation (SD). Student’s t-tests for two-group comparisons were performed to determine the statistical significance (P<0.05).

Results and discussion
Characterization of CK mixed micelles
The sizes and morphology of CK mixed micelles are illustrated in Figure 1. The average size of CK mixed micelles was 30.28±4.15 nm with a low polydispersity (Figure 1A). The CK mixed micelles had the highest negative zeta potential (~27.1±2.84 mV). The morphological images showed that CK mixed micelles were nanometer sized and spherical (Figure 1B). The drug LC was 13.26%±1.89% with a high entrapment efficiency (91.34%±5.24%). The solubility of CK increased from 35.2±4.3 to 1,463.2±153.3 µg/mL after CK AP/TPGS mixed micelle formation. Both the sizes of CK mixed micelles and the solubility of CK exhibited no significant decrease in 7 days. This shelf life could result in much convenience for the CK mixed micelles’ application. Furthermore, in vitro, a significantly higher release was reported for free CK group than that for CK mixed micelles, as shown in Figure 1C. This may be due to surface PEGylation and controlled release of mixed micelles group.

In vitro cellular uptake
Both fluorescence microscopy and confocal microscopy were used to confirm the uptake of mixed micelles in tumor cells by taking advantage of the intrinsic fluorescence of coumarin-6 and DAPI as the fluorescent probes. Figures 2 and 3 show that the nuclei of A549 cancer cells were stained blue with DAPI, while the cytoplasm was stained green with coumarin-6. After incubation with coumarin-6 for 4 h, the fluorescence images of A549 cell lines were photographed. In the free CK coumarin-6 group, the cytoplasm showed decreased green fluorescence. However, for the coumarin-6 mixed micelles group, the images showed a more intense fluorescence in cytoplasm. The observation indicated that mixed micelles could promote drug uptake. However, there was no significant accumulation of coumarin-6 in the cell nuclei.

In vitro cytotoxicity
The results for in vitro cytotoxicity are shown in Figure 4A; both free CK and CK mixed micelles have dose-dependent inhibitory effects on the viability of A549 cells. CK mixed micelles showed noticeable cytotoxicties in A549 tumor cells after 24 h incubation. The inhibition efficacy of CK mixed micelles against cell proliferation is better than that of free CK. The half-maximal inhibitory concentration (IC₅₀)
of free CK and CK mixed micelles at 24 h was 16.11±1.23 and 10.29±1.17 µg/mL, respectively. The results showed that formation of CK mixed micelles could increase the antitumor activity of CK. However, a similar tendency was not observed for CK release, which suggests that the improved antitumor effect of CK mixed micelles could likely be attributable to improved drug delivery instead of drug release.

**TUNEL assay**

The TUNEL assay was used to evaluate the DNA damage in situ. Its indication of apoptosis could specifically infer DNA strand breaks in cells. As shown in Figure 4B, both free CK and CK mixed micelles significantly induced cell apoptosis as revealed by cells with brown-stained nuclei as compared with control (P<0.05), while the normal cells were stained blue and had a low apoptosis index. In the CK micelle group, the apoptosis index was 45±5.25%, which is significantly larger than that in the CK group (17.28±2.25%), also indicating that mixed micelle nanocarriers exhibited better apoptosis effect to promote the antitumor effect.

**Apoptosis in A549 cells**

Next, to further analyze apoptosis, flow cytometry was chosen to quantify the proportion of cells in early and late apoptosis. As shown in Figure 5, the apoptosis percentage in the CK mixed micelles was significantly higher than that in the CK group, indicating that mixed micelle nanocarriers could effectively deliver CK to cells and induce apoptosis.

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**Figure 1** Droplet size (A), morphology (B) of CK mixed micelles, and its release in vitro (C).

**Note:** n=3, mean ± SE.

**Abbreviations:** CK, compound K; SE, standard error; h, hours.

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**Figure 2** Fluorescence microscopy of A549 cell following 4 h of treatment with C-6 or C-6 mixed micelles (n=3).

**Abbreviations:** C-6, coumarin-6; DAPI, 4′,6-diamidino-2-phenylindole; h, hours.

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**Figure 3** Confocal microscopy of A549 cell following 4 h of treatment with C-6 or C-6 mixed micelles (n=3).

**Abbreviations:** C-6, coumarin-6; DAPI, 4′,6-diamidino-2-phenylindole; h, hours.
late-stage apoptosis. As shown in Figure 4C, in the control group, the proportion of late-stage apoptotic A549 cells was 2.63%±0.28%. No significant apoptosis was observed in the control group. On the contrary, the proportion of late-stage apoptotic cells for free CK and CK mixed micelles was 7.34%±1.51% and 16.59%±2.83%, respectively, which indicates a significant increase. The tendency of early apoptosis was similar to late apoptosis mentioned earlier. Thus, CK mixed micelles were found to induce cell apoptosis markedly both in early and late stages of apoptosis compared with CK group.

**Cell cycle distribution in A549 cells**
The other possible effect of CK and CK mixed micelles was investigated. The percentage of cells in phase of cell cycle was significantly altered by CK or CK mixed micelles (Figure 5A). The micelles induced G0/G1 arrest in rapidly dividing cells, eventually resulting in better effect than CK.

**Cell migration assay**
Wound-healing assay was used to evaluate the effect on cell migration. The untreated group had a small wound after 24 h, but for the CK or CK mixed micelles group, a large wound was observed, indicating significant migration inhibition (Figure 5B). Thus, the CK mixed micelles exhibited better antimigration effect than CK.

**Near-infrared fluorescence imaging**
As seen in Figure 6, in vivo fluorescent optical imaging revealed weak fluorescence intensity in the tumor tissue for the DiR group, while in the DiR mixed micelles group, the fluorescence intensity significantly increased. DiR mixed
micelles displayed better targeting efficiency compared to free DiR, as evidenced by the fluorescence at 2 h after injection and maximum absorbance at 8 h. Furthermore, DiR mixed micelles exhibited low clearance until 24 h with strong fluorescence in tumor tissue. It can be inferred that DiR mixed micelles possessed better tumor targeting with a prolonged circulation effect. To further confirm the tissue distribution, ex vivo imaging of major tissues was performed and showed that the uptake of DiR by the tumor cells increased up to 24 h from the mixed micelles due to the targeting effect.

**Assessment of in vivo therapeutic efficacy**

At the end of the experiment, the tumor volumes of the CK or CK mixed micelles group were all notably lower than those of the control group (Figure 7A and B). A significant difference in tumor volumes was observed among all groups. The CK mixed micelles exhibited the maximal antitumor effect (66.24±8.77% at day 15). In order to evaluate the adverse effects of CK or CK mixed micelles, body weight was also recorded during the experiment. No significant changes in average body weight were observed until day 15.

**Figure 5** Cell cycle analysis assay (green G1, brown S, and blue G2 phase). (A) and wound healing assay (B) on AS49 cell.

**Notes:** n=3, mean±SE. Scale 50 µm.

**Abbreviations:** CK, compound K; SE, standard error.

**Figure 6** In vivo imaging studies for tumor targeting ability of DiR mixed micelles (n=3).

**Abbreviations:** DiR, 1,1′-dioctadecyl-3,3,3′,3′-tetramethylindotricarbocyanine iodide; h, hours.
The improved antitumor efficacy of CK mixed micelles in mice was further confirmed by histopathology analysis. H&E assay was chosen to further evaluate antitumor efficacy, hepatic toxicity, and renal toxicity (Figure 7C). CK mixed micelles exhibited the most effective antitumor activity. Morphological analysis of tumor slices of the CK mixed micelles group showed significant nuclear pyknosis and karyorrhexis, which indicate prominent apoptosis promoting effect consistent with the in vitro study. The pathological analysis of the liver and kidney showed no significant difference compared with the results observed for the control group. The abovementioned results show that the CK mixed micelles had better antitumor efficacy with lower hepato and renal toxicity.

As shown in Figure 8, treatment with CK mixed micelles significantly increased BAX expression and decreased Bcl-2 expression. Compared with the free CK group, the CK mixed micelles group showed almost 7.25-fold increase in BAX/Bcl-2 ratio. This indicated that CK mixed micelles could promote cell apoptosis via increased accumulation in tumor. The expression of caspase 3, caspase 8, and caspase 9 in tumor cells was detected to evaluate the upregulation of apoptosis sensitivity. The most favorable effect was observed in the CK mixed micelles group. The gray value of caspase 3, caspase 8, and caspase 9 increased by almost 100% in the CK mixed micelles group, compared to that in the free CK group. Interestingly, P-gp expression in tumors significantly decreased in the CK mixed micelles group, likely owing to the P-gp efflux inhibitory activity of TPGS.
At tumor sites, the overproduction of oxyradical has been reported. Mixed micelles contained antioxidants that may promote nanocarrier uptake by neutralizing the peroxides in tumor internal environment. This interaction could decrease oxidative stress and promote treatment efficacy at tumor sites. Moreover, unlike most normal vasculature, tumor vasculature has prevalent leaky vascular endothelium because of uncontrolled growth. Nanoparticles can effectively pass through the tumor vasculature because of the enhanced permeability and retention effect. In addition, particles with a diameter range of ~10–30 nm can avoid the accelerated blood clearance phenomenon and accordingly realize the prolonged circulation effect. Furthermore, PEGylation on the surface of mixed micelles can increase the uptake and circulation in vivo. Therefore, according to the abovementioned effects, the AP/TPGS mixed micelles were easily extravasated at tumor sites for passive targeted effect with prolonged circulation to increase antitumor effect in vivo. However, the use of AP as an antioxidant for facilitating targeted tumor tissue needs further research.

Conclusion
We aimed to evaluate the anticancer function and mainly focus on the promotion of apoptosis, cellular uptake, and tumor targeted effect of CK AP/TPGS mixed micelles. The in vitro and in vivo studies both indicated that the antitumor effect of the CK increased following the formation of the AP/TPGS mixed micelles. Therefore, AP/TPGS mixed micelles of CK could be a potential alternative for effective and targeted tumor therapy.

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Disclosure
The authors report no conflicts of interest in this work.

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