Evaluation of Thiel cadaveric model for MRI-guided stereotactic procedures in neurosurgery

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INTRODUCTION

The use of computer-assisted neurosurgery is an established technique in functional neurosurgical procedures such as treatment of Parkinson’s disease,[1-3,8,29,30] dystonia,[31] tremor[32] and craniootomy for intracranial lesions,[12] and gaining support in the treatment of epilepsy,[13,31] chronic pain,[14,16] and psychiatric disorders.[20,26] These procedures include ablative procedures such as thalamotomy,[14] pallidotomy,[18,38] anterior cingulotomy, anterior capsulotomy, and lesionectomy[12] or neurostimulation such as deep brain stimulation (DBS).[1,5,8,9,13,17,18,20,26,29,31] The main techniques used to generate stereotactic ablative procedures are stereotactic radiofrequency thermal lesioning or stereotactic radiosurgery (SRS). High frequency focused ultrasound (HFFUS), in contrast, is a newer less-invasive technique using ultrasonic energy to thermally ablate a target in the brain. All these techniques are performed without real time feedback or real time anatomical monitoring of the exact size and location of
the lesion or the implant. Computer-assisted magnetic resonance imaging (MRI)-guided focused ultrasound (MgfUS) and MRI-guided DBS implantation are techniques where the exact size or location of the lesion or the implant can be monitored in real time and the size of the lesions can be tailored to the individual patient.

As surgical training is becoming more formalized and had to be delivered in a much shorter time frame, future neurosurgeons may benefit immensely from practicing and mastering their craft in as real as possible scenario before performing these procedures on patients. Furthermore, mentors, trainers, and assessors in neurosurgery are under pressure to ensure that neurosurgeons of the future are competent to perform these procedures. We therefore evaluated Thiel cadavers as a model for computer-assisted MRI-guided functional neurosurgery.

MATERIALS AND METHODS

The study involved Thiel embalmed human cadavers, donated to the Centre for Anatomy and Human Identification at the University of Dundee for medical education and research in accordance to the UK-Anatomy Act (2006). The study was approved by the ethical board responsible for governance of Thiel cadaver program. Table 1 summarizes the background characteristics of cadavers that were used in these procedures. Four cadavers were over 83 years of age at the time of death and the average death to embalming was 72 h (24-144 h). On average the cadavers were in use for 9.4 months (4-15 months) before they were used in this study.

In order to assess the quality of the Thiel cadaver’s brain, MRI was used to screen each cadaver prior to its use. MRI scans were performed using 1.5 Tesla GE HDx MRI-machine (Milwaukee, WI). Two sequences were obtained using 8-channels head coil; T2-weighted sequence (TE 89 ms, TR >4000, bandwidth 20.8 kHz) to evaluate the anatomical integrity of the Thiel brain and Fiesta sequence (TE 4.2 ms, TR 7.1 ms, bandwidth 62.5 kHz) to assess amount of air bubbles in the brain.

Table 1: Summary of Thiel cadavers characteristics

| Cadaver | Age before death | Gender | Cause of death                  | Death to embalming (hours) | Time from embalming to use |
|---------|------------------|--------|---------------------------------|---------------------------|---------------------------|
| 1       | 87 years         | Female | Coronary heart disease          | 24                        | 15 months                 |
| 2       | 84 years         | Female | Cerebrovascular event and sepsis| 72                        | 10 months                 |
| 3       | 92 years         | Female | Congestive heart failure        | 144                       | 12 months                 |
| 4       | 89 years         | Male   | Congestive heart and renal failure | 72                      | 4 months                  |
| 5       | 64 years         | Female | Non-small cell lung cancer      | 48                        | 6 months                  |

To study the use of focused ultrasound (FUS) in these cadavers we performed craniotomies to overcome bone and enable us to use the FUS body system. The location of the craniotomies was selected on the basis of providing direct trajectory to the basal ganglia without traversing the ventricle or major sulci. The craniotomies were cited in the frontoparietal area. A skin flap was first raised, followed by drilling four burr holes using standard neurosurgical air driven craniotome. The dura matter was then carefully dissected off the inner surface of the skull to establish clear path between each adjacent burr holes. The cutting craniotome was used to cut the bone between each adjacent burr holes avoiding opening the dura matter and avoiding ingress of air into the intradural cavity. After the bone flap was removed, the craniectomy bone defect above the dura was filled with ultrasonic gel for coupling the ultrasonic probe. Throughout the procedure, the head was fixed using MRI-compatible surgical suite head clamp (GE, Milwaukee, WI).

We evaluated the quality of MRI images, assessed air bubbles, positioning of FUS probe, thermal spot shape produced by computer-assisted MgfUS, influence of aperture (ratio between the transmitting radius and focal distance of FUS) and effect of increasing the acoustic energy on temperature-rise and tissue displacement. Then we assessed cavitation thresholds induced by computer-assisted MgfUS. We also ran three workshops to implant DBS using MRI guidance and SurgiVision ClearPoint system.

Computer-assisted MgfUS and MRI-thermometry

Computer-assisted MgfUS was performed with ExAblate 2100 Conformal Bone System (InSightec Ltd, Tirat Carmel, Israel) inside 1.5 Tesla MRI (GE, Milwaukee, WI). The FUS system consisted of 1000 elements array transducer with central frequency of 0.55 MHz. The system allows sonications under MRI Proton Resonance Frequency (PRF) according to the following equation: \( \Delta T = \Delta \Phi / \alpha T E B \), where \( \Delta T \) is the difference in temperature, \( \Delta \Phi \) is the phase shift, \( \gamma \) is the gyromagnetic ratio, TE is the repetition time, \( B_0 \) is the magnetic field strength, and \( \alpha \) is a PRF coefficient. In order to assess the tissue response to different physical applications of FUS, a total of 50 sonications were performed on cadavers 2 and 3, using different apertures, different sites in the brain, and different acoustic power levels.

MRI-acoustic radiation force imaging

MRI-Acoustic radiation force imaging (ARFI) sequence described by Hertzberg et al.\(^{[15]}\) was used to assess tissue displacement of the cadaveric brain. Three different acoustic power levels were used.

Quality assurance

Thermal spot shape and the level of heating of the Conformal Bone System were assessed in a phantom for quality assurance, the thermal spot shape and heating changed according to the location of the thermal spot.
Therefore, the same sonications in the same locations as in cadavers were performed in tissue mimicking phantom for comparison purposes. The tissue-mimicking phantom is part of the ExAblate system tool-kit and is regularly used for daily Quality Assurance (QA) procedures prior to computer-assisted MgfUS interventions.

**Cavitation threshold**

During transmission of ultrasound energy, one of the ultrasonic channels of conformal bone transducer was used as a receiver, collecting reflected signals. Cavitation is a process, where micro-bubbles (gas cavities) are formed due to ultrasonic application. There are two types of cavitation; stable and transient. Stable cavitation defined as gas bubble's oscillation, changing its size and shape according to ultrasonic wave application. This cavitation has an acoustical signature, which can be recorded in frequency domain and is seen as peaks in multiplications (or divisions) of the main transmitting frequency. Transient cavitation is a phenomenon, where the gas bubbles can no longer sustain its size and violently collapse, causing mechanical distraction, rather than thermal ablation. Transient cavitation is seen as a broad-band noise on the frequency domain. As a result of this definition it is expected that the threshold for transient cavitation will be higher than that required for stable cavitation. Figure 1 depicts three types of sonication recordings as seen on the ExAblate 2100 spectrum measurement; no cavitation, stable cavitation, and transient cavitation.

In order to assess cavitation thresholds in this model, sonication with increasing acoustic power levels to determine the cavitation threshold for stable and transient cavitation was performed.

**RESULTS**

**Magnetic resonance imaging**

The quality of brains depicted by MRI imaging was excellent with good preservation of white gray matter differentiation as seen in Figure 2. The images were of good quality to be used in both the ExAblate and ClearPoint planning software systems. In addition, there were no concentrations of visible air bubbles.

**Tissue handling**

The scalp and bone qualities of Thiel cadavers were excellent. They both handled very well with similar properties to in vivo procedures as Thiel embalmment techniques preserves cadavers in away the tissues remain soft. The dura matter was often adherent to the inner table of the skull consistent with advanced age of the subjects. Therefore extra care during dissection of the dura matter from the bone was necessary to avoid dural penetration.

**Sonication**

Thiel embalmed brains proved to have linear dependence of applied acoustic energy to thermal rise [Figure 3]. In addition, Thiel embalmed brains had linear dependence of tissue displacement as a function of applied power [Figure 4]. The thermal spot shape resembled the spot shape produced in tissue mimicking phantom, moreover, aperture dependence also resembled the sonications in phantom [Figure 5].

**Cavitation threshold**

Cavitation threshold was found to be 40 Acoustic Watt for stable cavitation and 60 Acoustic Watt for transient cavitation. Given the sonication location and applied acoustic power, these values are compliant to mechanical index (MI) of 4.3 and 5.3, respectively. However, once the transient cavitation threshold was reached at certain location, transient cavitation was observed at the same location.

**Postprocedure MRI assessment**

One major advantage of MgfUS is immediate postprocedure evaluation. Thiel cadaver in these experiments enabled postprocedures evaluation of the location and size of the lesion. Figure 6 depicts immediate postprocedure results [Figure 6].

**MRI-guided DBS implantation**

It was possible to teach residents to implant DBS in Thiel cadavers using MRI guidance and the Surgi-Vision ClearPoint system.
DISCUSSION

MRI imaging of Thiel embalmed cadaveric brains suggests great preservation of the brain tissue and revealed suitable imaging characteristics with clear differentiation between white and gray matters. The long-term usability of these cadavers up to 15 months makes the Thiel embalmed cadaver an excellent model for any other computer-assisted image-guided minimally invasive neurosurgery for training, such as DBS insertion. Life-like tissue flexibility simulates operative procedures in the operation room and far exceeds the properties of formalin-embalmed cadavers\[11\] and equals the quality of fresh cadavers without the constraints of rapid decay and infection risk. Other authors found similar advantages of Thiel cadavers in extracranial applications\[6,14,16,20-24\]. The ability to focus the ultrasonic beam and linear temperature and displacement behavior of the Thiel cadaveric brain tissue suggests that Thiel embalmed cadavers can be used for developing and testing various stereotactic functional neurosurgical procedures and establishing treatment envelope limits, focusing algorithms, and skull heating effects using HFFUS. However, there was significant difference of MRI-temperature mapping between sonications of Thiel embalmed brain tissue and tissue mimicking phantom. This can be explained by the fact that the PRF coefficient ($\alpha$) is different between normal brain because of its increased water content and cerebral perfusion and Thiel

Figure 2: MRI imaging of the brain of Thiel embalmed cadaver 3. a,c -T2-weighted Fast Spin Echo (TR/TE=89.9/7560 ms, bw=20.8 kHz). b, d-FIESTA pulse sequence (TR/TE=4.2/7.3 ms, BW=62.5 kHz)

Figure 3: Graph of thermal rise as a function of applied acoustic energy, performed on Cadaver 3

Figure 4: MR-ARFI, a-graph of displacement as a function of applied acoustic power and b-displacement map for applied acoustic power of 100 W (applied on Cadaver 3)
preservation fluid. Another possible explanation is that the embalming process could change the heat capacity properties of the brain and its elasticity. Future testing needs to be calibrated and scaled to fit the in vivo tissue behavior. The relatively low cavitation threshold is in line with the work of Benkhadra et al.,[7] who observed a higher echogenicity of the Thiel embalmed cadavers compared with fresh cadavers. The authors believe that improved embalmment and storage processes dedicated to this purpose would reduce this threshold. Nevertheless the ability to create cavitation can be used for transcranial cavitation studies. For most training and testing purposes, postprocedure assessment can be achieved by immediate MRI imaging. Future Thiel embalmed tissue characterization, PRF coefficient measurements, and embalming techniques are currently being investigated and likely to answer these questions. Several groups already reported small series using computer-assisted MgUS to treat functional and other conditions such as tumors.[10,21,25,28] As computer-assisted MgUS applications emerge, it is important to study its effects in as real as possible conditions and provide a platform for training and assessing competence in these procedures. Thiel cadavers using Thiel embalment techniques[12,31] provides better and more realistic operative and positioning conditions compared with animal models.[10,21,27,28] We used this model to run three successful MRI-guided DBS implantation courses to train residents as an example of using it as a model in teaching and learning MRI-guided stereotactic procedures.

CONCLUSIONS

A Thiel embalmed cadaveric model to develop, assess, and monitor minimally invasive computer-assisted MgUS neurosurgical procedures and to train residents in MRI-guided DBS implantation was developed. Thiel embalmed cadaveric brains are anatomically matched model for any computer-assisted MR-guided brain-related minimal intervention procedures.

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