Total variation-based phase retrieval for diffraction tomography

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In optical diffraction tomography (ODT), the three-dimensional scattering potential of a microscopic object rotating around its center is recovered by a series of illuminations with coherent light. Reconstruction algorithms such as the filtered backpropagation require knowledge of the complex-valued wave at the measurement plane, whereas often only intensities, i.e., phaseless measurements, are available in practice.

We propose a new reconstruction approach for ODT with unknown phase information based on three key ingredients. First, the light propagation is modeled using Born’s approximation enabling us to use the Fourier diffraction theorem. Second, we stabilize the inversion of the non-uniform discrete Fourier transform via total variation regularization utilizing a primal-dual iteration, which also yields a novel numerical inversion formula for ODT with known phase. The third ingredient is a hybrid input-output scheme. We achieved convincing numerical results, which indicate that ODT with phaseless data is possible. The so-obtained 2D and 3D reconstructions are even comparable to the ones with known phase.

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1 Introduction

Illuminating three-dimensional (3D) objects from different angles, we are interested in tomographic reconstructions. In classical X-ray computerized tomography, the light is assumed to propagate along straight lines enabling reconstruction via the inverse Radon

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transform. This assumption relies on the fact that the employed X-rays have a very short wavelength, which is much smaller than any object features of interest. In \textit{optical diffraction tomography} (ODT), the image is obtained via visible light of wavelengths of hundreds of nanometers being the size of studied features such as subcellular structures. Therefore, we rely on a more sophisticated light propagation model taking the occurring diffraction into account.

Mathematically speaking, we aim to recover the three-dimensional scattering potential of the unknown object given two-dimensional measurements of the complex wave function at a plane behind the object for different illumination directions. We assume that the illumination directions are known beforehand, motion detection methods were discussed in [20]. To model the light propagation, we take advantage of the Born approximation, which is valid for objects of small size and variation of the scattering potential. A well-established inversion method for the Born-based ODT model is the backpropagation [17], which is still widely used in practice [22, 54]. The backpropagation, however, relies on complex-valued measurements whereas only phaseless intensities are available in most practical setups. This means that the object reconstruction becomes more ill posed and is coupled with a phase retrieval problem.

Phase retrievals of different kinds have been intensely studied in the literature. In general, solutions are highly ambiguous. Characterizations of the whole solution set and uniqueness guarantees under additional constraints like known support or non-negativity have been studied for functions with continuous domains [1, 34, 46, 47, 60], where the measurements correspond to the intensity of the Fourier transform. Analogous results exist for fractional Fourier intensities [41] for instance. Even if the Fourier phase retrieval problem is discretized, the ambiguousness remains an issue independently of how many measurements are available [3, 6–8, 19, 34]. To overcome these problems, more general phase retrieval problems, where the intensity of arbitrary linear measurements are given, have been studied. Under certain assumptions on the linear measurements, the phase retrieval problem becomes unique [11, 12, 23, 24]. Using a tensorial lifting, the problem may be exemplarily solved using semi-definite programming [11, 12], tensor-free primal-dual methods [5], or polarization techniques [2, 56]. Moreover, the phase retrieval problem is well understood in the context of frames [2, 34, 56].

Unfortunately, phase retrieval in ODT does not fit in the above setups since the given measurements with respect to the Born approximation are non-linear. Therefore, the well-established theoretical results regarding ambiguousness, uniqueness, and stability cannot be transferred to our problem. In X-ray tomography, where the intensity measurements are modeled using the Radon transform of the unknown object followed by diffraction, uniqueness of the reconstruction is guaranteed [53]. The difference in the employed mathematical model, however, prevents a direct application of the uniqueness results in ODT.

For retrieving an unknown phase in ODT, different approaches have been studied. An iterative method of propagation and backpropagation in free space between the measurements plane and a parallel plane through the object was proposed by Maleki and
Devaney [52]. The Gabor holography compared unfavorably in numerical tests [62]. A phase retrieval method utilizing ideas of Fourier ptychography was developed in [40]. Other approaches rely on the acquisition of more data using two parallel measurement planes [30] or the phase shifting interferometry (PSI) requiring 4 intensity images per illumination direction. Furthermore, phase retrieval based on a far zone approximation of Born [14] or using the X-ray transform [35] has been studied.

In this paper, we consider the phase retrieval problem in ODT, where the absolute value of the wave is measured at one plane per illumination direction, and we assume that the Born approximation is valid. Our proposed method is based on the hybrid input-output algorithm from Fourier phase retrieval combined with a total variation (TV) regularization utilizing a primal-dual method. TV regularization has already been applied to limited angle reconstruction in ODT utilizing an approximate Radon transform [50].

The main contributions of this paper are as follows:

- We consider the inverse nonuniform discrete Fourier transform (NDFT) as an inverse problem and apply TV-based regularization methods to improve the inversion especially in the presence of noise. We apply this regularized NDFT inversion to obtain a novel reconstruction method for ODT with known phase.

- We propose a numerical algorithm for solving the phase retrieval problem in ODT. This algorithm makes use of an adaption of the hybrid input-output scheme and the TV-regularized inversion of the NDFT.

- Our numerical simulations indicate that phase retrieval is possible and greatly benefits from the regularized ODT inversion. In total, the reconstruction quality is comparable to the known-phase inversion.

Outline of the paper. The employed notation is introduced in Section 2. The basics on diffraction tomography and the theoretical foundation of the inversion methods are explained in Section 3. We introduce the discretized setting used for implementations in Section 4. Since the inversion of the NDFT is the key element for reconstruction in diffraction tomography, we discuss different computation methods for the inverse NDFT in Section 5. On the basis of these methods, different numerical ODT inversions for complex-valued data are studied and compared. The proposed phase retrieval method for ODT is derived in Section 6. Finally, numerical simulations in Section 7 show that phase retrieval in ODT is possible and we achieve favorable reconstruction results. Conclusions are given in Section 8.

2 Notation and preliminary remarks

In the following, we use the (symmetric) index set

$$\mathcal{I}_K := \{-K/2, -K/2+1, \ldots, K/2-1\},$$
where $K \in 2\mathbb{N}$. Although $I_K$ may be adapted for odd $K$, we only consider the even case for convenience. The set of the first $M \in \mathbb{N}$ positive integers is further denoted by

$$J_M := \{1, 2, \ldots, M\}.$$ 

Numerically, we represent the unknown object as a $d$-dimensional signal

$$x := [x_k]_{k \in I_K^d} \in \mathbb{R}^{K^d},$$

which may be interpreted as samples of a multivariate function. The (weighted) $2$-norm of the $d$-dimensional signal $x$ is defined by

$$\|x\|_2 := \sum_{k \in I_K^d} |x_k|^2 \quad \text{and} \quad \|x\|_{2,w} := \sum_{k \in I_K^d} w_k |x_k|^2$$

for some non-negative weights $w \in \mathbb{R}_0^{K^d}$.

Besides the signals, we also require the notion of a $d$-dimensional discrete vector field $y \in \mathbb{R}^{K^d \times d}$, where the elements of $y$ are itself $d$-dimensional vectors, i.e. $y_k \in \mathbb{R}^d$ for $k \in I_K^d$. The signal $y,\ell$ consisting of the $\ell$th components is defined by $[y,\ell]_k := [y_k]_\ell$ for $k \in I_K^d$ and $\ell \in J_d$. The $(1,2)$- and $(2,2)$-norm of a discrete vector field is given by

$$\|y\|_{1,2} := \sum_{k \in I_K^d} \|y_k\|_2 \quad \text{and} \quad \|y\|_{2,2} := \sum_{k \in I_K^d} \|y_k\|_2^2.$$

We use analogous definitions for signals whose domains are not $I_K^d$.

Finally, we interpret all occurring complex vector spaces $\mathbb{C}^N$ as $2N$-dimensional vector spaces over $\mathbb{R}$ with the inner product

$$\langle x, y \rangle := \sum_{n=1}^N \text{Re}[x_n y_n]$$

for $x, y \in \mathbb{C}^N$, which is necessary to apply certain techniques and numerical methods from convex analysis. For $A \in \mathbb{C}^{N \times K}$ declaring the mapping $x \mapsto Ax$ from $\mathbb{R}^K$ to $\mathbb{C}^N$, the adjoint mapping becomes $y \mapsto \text{Re}[A^*y]$ from $\mathbb{C}^N$ to $\mathbb{R}^K$.

## 3 Diffraction tomography

In this section, we describe the setup in optical diffraction tomography (ODT), cf. [45].

We want to reconstruct an object’s scattering potential $f : \mathbb{R}^d \rightarrow \mathbb{R}$, where we restrict our considerations to the practically meaningful dimensions $d \in \{2, 3\}$. The object is embedded in a homogeneous background and is illuminated by a monochromatic plane wave. The incident field

$$u^{\text{inc}}(x) = e^{ik_0 x_d}, \quad x \in \mathbb{R}^d,$$  

(1)
Figure 1: Experimental setup for $d = 3$ with measurement plane located at $x_3 = r_M$.

with wave number $k_0 > 0$ propagates in the direction of $x_d$.

For the tomographic reconstruction, we rotate the unknown object during the measurement process. The rotation at time $t \in [0, T]$ for $T > 0$ is described by the known rotation matrix $R_t \in \text{SO}(d)$. The rotated object has the scattering potential $f(R_t)$. The resulting total field at time $t$ is denoted by $u_t^{\text{tot}} : \mathbb{R}^d \to \mathbb{C}$. We decompose the total field into

$$u_t^{\text{tot}} = u_t^{\text{inc}} + u_t^{\text{sca}}$$

with the known incident field $u_t^{\text{inc}}$ given in (1) and the scattered field $u_t^{\text{sca}}$.

The total field $u_t^{\text{tot}}$ at time $t$ is measured at a fixed plane behind the object. More precisely, we detect either $u_t^{\text{tot}}(x', r_M)$ or $|u_t^{\text{tot}}(x', r_M)|$ for all $x' \in \mathbb{R}^{d-1}$ and a fixed $r_M > 0$; the measurement plane is thus orthogonal to the $x_d$ axis. Since the plane lies outside the object, $f$ is assumed to be bounded and compactly supported in the ball $B_{r_M} = \{ x \in \mathbb{R}^d : \| x \|_2 < r_M \}$. The experimental setup is illustrated in Figure 1.

### 3.1 Born approximation

To model the scattered wave $u_t^{\text{sca}}$, we employ the first order Born approximation [42], where $u_t^{\text{sca}}$ solves the Helmholtz equation

$$(\Delta + k_0^2) u_t^{\text{sca}} = -f u_t^{\text{inc}}. \quad (2)$$

Under the Sommerfeld radiation condition, which basically says that the scattered field is an outgoing wave, the Helmholtz equation (2) has a unique solution. This solution may be computed by using the outgoing Green function $G_d$ of the Helmholtz equation, see [16, Sect. 3.4] or [55, Sect. 3.3], which is given by

$$G_3(x) := \frac{e^{ik_0\|x\|_2}}{4\pi \|x\|_2}, \quad x \in \mathbb{R}^3 \setminus \{0\},$$
and
\[ G_2(x) := \frac{i}{4} H_0^{(1)}(k_0 \|x\|_2), \quad x \in \mathbb{R}^2 \setminus \{0\}, \]
where \( H_0^{(1)}(x) := (\pi i)^{-1} \int_{-\infty}^{\infty} e^{ix \cosh t} \, dt, \ x > 0, \) denotes the zeroth order Hankel function of the first kind \([33, (8.421.1)]\). The scattered field \( u_t^{\text{sca}} \) is then given by the convolution
\[ u_t^{\text{sca}}(x) = [(f(R_t) u^\text{inc}) * G_d](x) := \int_{\mathbb{R}^d} f(R_t y) u^\text{inc}(y) G_d(x - y) \, dy, \quad x \in \mathbb{R}^d. \] (3)
Restricting the convolution to the measurement plane, we model the given ODT data using the (non-linear) forward map \( D^\text{tot} \) defined by
\[ D^\text{tot} f(x', t) := [(f(R_t) u^\text{inc}) * G_d](x', r_M) + u^\text{inc}(r_M), \quad x' \in \mathbb{R}^{d-1}, \ t \in [0, T]. \] (4)

### 3.2 Fourier diffraction theorem

Besides the convolutional representation (4), the forward map \( D^\text{tot} \) may be represented using the Fourier transform, which significantly simplifies the inversion. The \( d \)-dimensional **Fourier transform** is defined by
\[ \mathcal{F}[f](y) := (2\pi)^{-d/2} \int_{\mathbb{R}^d} f(x) e^{-ix \cdot y} \, dx, \quad y \in \mathbb{R}^d, \] (5)
and the **partial Fourier transform** with respect to the first \( d-1 \) coordinates by
\[ \mathcal{F}_{1,\ldots,d-1}[f](y', x_d) := (2\pi)^{-(d-1)/2} \int_{\mathbb{R}^{d-1}} f(x', x_d) e^{-ix' \cdot y'} \, dx' \] (6)
for \((y', x_d) \in \mathbb{R}^{d-1} \times \mathbb{R}^1\). Recalling that \( k_0 \) is the wave number of the incident field, we further define
\[ \kappa(y') := \sqrt{k_0^2 - \|y'\|_2^2} \quad \text{and} \quad h(y') := \left( \frac{y'}{\kappa(y')}, -k_0 \right) \in \mathbb{R}^d. \]
where \( y' \in B_{k_0}^{d-1} \). The **Fourier diffraction theorem** [42, 55] now states
\[ \mathcal{F}_{1,\ldots,d-1}[u_t^{\text{sca}}](y', r_M) = \frac{i}{\sqrt{2\pi} \kappa(y')} e^{i\kappa(y') \cdot r_M} \mathcal{F}[f](R_t h(y')), \quad y' \in B_{k_0}^{d-1}, \ t \in [0, T]. \] (7)
In general, the identity (7) only holds in a distributional sense [45]. Geometrically, the set \( \{h(y') : \|y'\|_2 < k_0 \} \) is a semisphere or semicircle, whose center is on the negative \( x_d \) axis, and which passes through the origin. On the right-hand side of (7), we thus evaluate the Fourier transform \( \mathcal{F}[f] \) on a rotated semisphere or semicircle; on the left-hand side, partial Fourier transforms of the measurements \( u_t^{\text{sca}}(\cdot, r_M) \) are computed.
3.3 Uniqueness of the reconstruction

Under certain conditions, the scattering potential \( f \) is uniquely determined by the given measurements of \( u^\text{tot}_t \). The following uniqueness result is based on the Paley–Wiener theorem [39, Thm. 7.3.1].

**Proposition 3.1 (Paley–Wiener)** Let \( f \in L^1(\mathbb{R}^d) \) have compact support. Then the Fourier transform \( F[f] \in C(\mathbb{R}^d) \) is uniquely extendable to an analytic function on \( \mathbb{C}^d \).

**Theorem 3.2 (ODT inversion)** Let \( f \in L^1(\mathbb{R}^d) \) have a compact support in \( B^{d}_{r_M} \), and let the Lebesgue measure of \( Y := \{ R_t h(y') : y' \in B^{d-1}_{k_0}, t \in [0, T] \} \subset \mathbb{R}^d \) be positive. Then \( f \) is uniquely determined by \( D^\text{tot}[f] \) in (4).

**Proof:** Given \( u^\text{tot}_t \), we have \( u^\text{sca}_t = u^\text{tot}_t - e^{i k_0 r_M} \). By the Fourier diffraction theorem (7), we obtain \( F[f] \) on \( Y \), which has positive Lebesgue measure. Any \( d \)-variate analytic function is uniquely determined by its values on a set of positive Lebesgue measure [49, Sect. 4.1]. Since \( F[f] \) is an analytic function by Proposition 3.1, \( F[f] \) is uniquely determined on \( \mathbb{R}^d \) and thus \( f \) itself due to the uniqueness of the Fourier transform [57, Thm. 4.47].

The requirements of Theorem 3.2 are, for instance, fulfilled if \( R_t \) describes a full rotation around an axis different from \( x_3 \) in 3D, or if the rotation angle covers an interval in 2D.

4 Discretization

The mapping \( D^\text{tot} \) and its inversion can be numerically realized utilizing the Fourier diffraction theorem (7). For this purpose, we first restrict the total field \( u^\text{tot}_t \) or, more precisely, the scattered field \( u^\text{sca}_t \) to the cube \([-L_M, L_M]^{d-1}\) and then discretize the fields using \( N \in 2\mathbb{N} \) samples for each spatial direction and \( M \in \mathbb{N} \) time steps, cf. [45]. On the uniforms grids

\[
z'_n := \frac{2L_M}{N} n, \quad n \in \mathbb{I}_N^{d-1} \quad \text{and} \quad t_m := \frac{T}{M} m, \quad m \in \mathbb{I}_M,
\]

the scattered fields \( u^\text{sca}_t(z', r_M) \) are represented by the vectors

\[
v^\text{sca}_m := [v^\text{sca}_{m,n}]_{n \in \mathbb{I}_N^{d-1}} \quad \text{with} \quad v^\text{sca}_{m,n} := u^\text{sca}_m(z'_n, r_M).
\]

The \((d-1)\)-dimensional discrete Fourier transform (DFT) of \( v^\text{sca}_m \) is given by

\[
[F_{\text{DFT}} v^\text{sca}_m]_{\ell} := \sum_{n \in \mathbb{I}_N^{d-1}} v^\text{sca}_{m,n} e^{-2\pi i \ell n/N}, \quad \ell \in \mathbb{I}_N^{d-1},
\]

\[
\text{(10)}
\]
and may be inverted using the inverse DFT
\[ y_m^{\text{scat}} = \frac{1}{N^{d-1}} \sum_{\ell \in \mathcal{I}_N^{d-1}} [F_{\text{DFT}} v_m^{\text{scat}}]_{\ell} e^{2\pi i n \cdot \ell / N}, \quad n \in \mathcal{I}_N^{d-1}. \] (11)

The left-hand side of the Fourier diffraction theorem (7) may thus be discretized as
\[ F_{1,\ldots,d-1} u_m^{\text{scat}} (y'_\ell, r_M) \approx (2\pi)^{-\frac{d}{2}} \left( \frac{2L_s}{N} \right)^{d-1} [F_{\text{DFT}} v_m^{\text{scat}}]_{\ell}, \quad \ell \in \mathcal{I}_N^{d-1}, \] (12)
where \( y'_\ell := \frac{\pi}{L_{\ell M}} \ell \) with \( \ell \in \mathcal{I}_N^{d-1} \), which provides an approximation of \( F[f] \) on the nonuniform grid
\[ \mathcal{Y}_{M,N} := \{ R_{r_m} h(y'_\ell) : m \in \mathcal{J}_M, \ell \in \mathcal{I}_N^{d-1}, \| y'_\ell \| < k_0 \}. \] (13)

For simplicity, we assume \( \| y'_\ell \|_2 < k_0 \) for all \( \ell \in \mathcal{I}_N^{d-1} \) and truncate the grid to the points satisfying this assumption.

For the right-hand side of the Fourier diffraction theorem, we assume \( \text{supp} f \subset [-L_s, L_s]^d \) and use \( K \in 2N \) sampling points per direction. Using the uniform grid
\[ x_k := \frac{2L}{K} k, \quad k \in \mathcal{I}_K^d, \]
we approximate the scattering potential \( f \) by
\[ f = [f_k]_{k \in \mathcal{I}_K^d} := [f(x_k)]_{k \in \mathcal{I}_K^d} \in \mathbb{R}^{K^d}. \]

The \( d \)-dimensional nonuniform discrete Fourier transform (NDFT) of \( f \) onto the set \( \mathcal{Y}_{M,N} \) is defined by
\[ [F_{\text{NDFT}} f]_{m,\ell} := \sum_{k \in \mathcal{I}_K^d} f_k e^{-i x_k \cdot (R_{r_m} h(y'_\ell))}, \quad m \in \mathcal{J}_M, \ell \in \mathcal{I}_N^{d-1}, \] (14)
which approximates the right-hand Fourier transform in (7) via
\[ F[f] (R_{r_m} h(y'_\ell)) \approx (2\pi)^{-\frac{d}{2}} \left( \frac{2L_s}{K} \right)^d [F_{\text{NDFT}} f]_{m,\ell}, \quad m \in \mathcal{J}_M, \ell \in \mathcal{I}_N^{d-1}. \] (15)

Inserting the approximations (12) and (15) into the Fourier diffraction theorem (7), we obtain
\[ (2\pi)^{-\frac{d}{2}} \left( \frac{2L_M}{N} \right)^{d-1} [F_{\text{DFT}} v_m^{\text{scat}}]_{\ell} \approx \frac{i \sqrt{\pi}}{\sqrt{2} \kappa(y'_\ell)} e^{i \kappa(y'_\ell) r_M} (2\pi)^{-\frac{d}{2}} \left( \frac{2L_s}{K} \right)^d [F_{\text{NDFT}} f]_{m,\ell}. \]

With the definition
\[ c = [c_{\ell}]_{\ell \in \mathcal{I}_N^{d-1}} \in \mathbb{R}^{N^{d-1}} \text{ with } c_{\ell} := \frac{i}{\kappa(y'_\ell)} e^{i \kappa(y'_\ell) r_M} \left( \frac{N}{L_M} \right)^{d-1} \left( \frac{L_s}{K} \right)^d, \]
the discrete Fourier diffraction theorem becomes
\[ [F_{\text{DFT}} v_{m}^{\text{scat}}]_{\ell} \approx c_{\ell} \left( F_{\text{NDFT}} f \right)_{m,\ell}. \]

Incorporating the incident field, we approximate \( D_{\text{tot}} \) in (4) by the discrete diffraction tomography map
\[
D_{\text{tot}}^{f} := F_{\text{DFT}}^{-1} (c \odot F_{\text{NDFT}} f) + e^{ik_{0}r_{M}}, \quad f \in \mathbb{R}^{K},
\]
where \( \odot \) denotes the Hadamard (entrywise) product of two matrices or vectors. The numerical computation of the discrete forward transform \( D_{\text{tot}}^{f} \) basically consists of an NDFT, an entrywise multiplication with \( c \), and a DFT, see Algorithm 1.

**Algorithm 1: Computation of \( D_{\text{tot}}^{f} \)**

**Input:** Scattering potential \( f = [f(x_{k})]_{k \in \mathcal{I}_{K}} \).

Compute the NDFT \( g := F_{\text{NDFT}} f \) by (14);

for \( m \in \mathcal{J}_{M} \) do
\[
\tilde{g}_{m} := c \odot g_{m}; \quad v_{m}^{\text{scat}} := F_{\text{DFT}}^{-1} \tilde{g}_{m},
\]
end

**Output:** Scattered wave \( u_{m,n}^{\text{tot}}(n, r_{M}) \approx v_{m,n}^{\text{scat}} + e^{ik_{0}r_{M}}, m \in \mathcal{J}_{M}, n \in \mathcal{I}_{N}^{d-1}. \)

The reconstruction of \( f \), see Algorithm 2, is basically an inverse of the forward transform. The first two parts are very simple to invert utilizing the DFT (11) and a pointwise division. However, the inversion of the NDFT is a more challenging problem that is covered in the following Section 5. A schematic overview about the reconstruction steps is provided in Figure 2.

**Algorithm 2: Inversion of \( D_{\text{tot}}^{f} \)**

**Input:** Scattered wave \( v_{m,n}^{\text{scat}} := u_{m,n}^{\text{tot}}(n, r_{M}) \) \( = e^{ik_{0}r_{M}}, m \in \mathcal{J}_{M}, n \in \mathcal{I}_{N}^{d-1}. \)

for \( m \in \mathcal{J}_{M} \) do
\[
\tilde{g}_{m} := F_{\text{DFT}} v_{m}^{\text{scat}}; \quad v_{m} := \tilde{g}_{m} \odot c, \text{ where } \odot \text{ denotes the Hadamard (entrywise) division};
\]
end

Compute the inverse NDFT by solving \( F_{\text{NDFT}} f = g \) for \( f \), see Section 5;

**Output:** Scattering potential \( f \approx [f(x_{k})]_{k \in \mathcal{I}_{K}} \).

The DFT (10) and its inverse (11) can be computed efficiently with the well-known fast Fourier transform (FFT) in \( \mathcal{O}(N^{d-1} \log N) \) operations. Furthermore, there are fast algorithms for the computation of the NDFT (14) known as nonuniform fast Fourier transform (NFFT), which provides an arbitrarily tight approximation of the NDFT and uses \( \mathcal{O}(K^{d} \log K) \) instead of the \( \mathcal{O}(K^{2d}) \) operations of the naive matrix-vector multiplication [9, 18, 59]. For our numerical simulations, we use the implementation of the NFFT [44] provided in the software package [43], which also includes a fast algorithm for the adjoint NDFT with the same arithmetic complexity.
The approximate inversion of the NDFT (14) is the most crucial part for the reconstruction in Algorithm 2. Let \( g \in \mathbb{R}^{MN^{d-1}} \) be given. An (approximate) solution \( f \in \mathbb{R}^{K^d} \) of

\[
F_{\text{NDFT}} f = g
\]  
(17)

is called an inverse NDFT of \( g \). There is no exact inversion formula known in general. Depending on the distribution of the nodes \( Y_{M,N} \), the inverse NDFT (17) might not have a unique solution or be ill-conditioned [57, Sect. 7.6.2].

### 5.1 Discrete backpropagation

The idea behind the backpropagation [17] is to apply a quadrature rule to the (continuous) inverse Fourier transform restricted to the set \( Y \) in (8), where values are available by the Fourier diffraction theorem (7). The continuous backpropagation is defined by

\[
(2\pi)^{-d/2} \int_Y \mathcal{F}[f](y) e^{iy \cdot x} \, dy, \quad x \in \mathbb{R}^d,
\]  
(18)

which is simply the inverse Fourier transform applied to \( 1_Y \mathcal{F}[f] \), where \( 1_Y(y) := 1 \) if \( y \in Y \) and zero elsewhere. Applying the substitution \((t,z') \mapsto y = R_t h(z') \) and a quadrature rule with nodes \((t_m,z'_n)\) and weights \( w = [w_{m,n}]_{m \in \mathcal{J}_M, n \in \mathcal{T}_N^{d-1}} \in \mathbb{R}_{>0}^{M N^{d-1}} \) to (18), we arrive at the discrete backpropagation (BP) \( B \) of \( g \), namely

\[
[Bg]_k := \sum_{m \in \mathcal{J}_M} \sum_{n \in \mathcal{T}_N^{d-1}} w_{m,n} g_{m,n} e^{-i(k \cdot \frac{z_n}{N} - (R_t h(z'_n))}, \quad k \in \mathcal{T}_K^d, \ n \in \mathcal{T}_N^{d-1}.
\]  
(19)
For many situations in ODT, the weights \( w \) are known analytically [45, Sect. 4]. For instance, if the 3D object makes a full turn around the \( x_1 \) axis with rotation angle \( t \in [0, 2\pi] \), we have the nodes (9) and weights

\[
w_{m,n} = \frac{k_0 |[z_n^*]_2| \ 2\pi k_0^2}{2\kappa (z_n^*)} \frac{1}{MN^2}, \quad m \in \mathcal{J}_M, \ n \in I_N^d.
\]

The discrete backpropagation is an adjoint NDFT, i.e. \( \mathbf{B}g = \mathbf{F}^*_\text{NDFT}(w \odot g) \), which can be efficiently evaluated via the adjoint NFFT.

### 5.2 Conjugate gradient method

Equation (17) is a linear equation system that may be solved in the least-square sense by applying the iterative conjugate gradient (CG) method. This approach has been successfully applied in ODT [25, 45] as well as in X-ray imaging [58], magnetic resonance imaging [48], or spherical tomography [38]. We consider the overdetermined case \( MN^{d-1} \geq K^d \). The underdetermined case is similar and covered in [51]. The idea is to find a solution \( f \in \mathbb{R}^{K^d} \) of

\[
\text{minimize} \quad \| \mathbf{F}_{\text{NDFT}} f - g \|_{2,w}^2
\]

with some weights \( w = [w_{m,n}]_{m \in \mathcal{J}_M, n \in I_N^d} \in \mathbb{R}_>^{MN^{d-1}} \). The classical CG method corresponds to the constant weights \( w_{m,n} = 1 \). Obviously, any exact solution \( f \) of (17) is a minimizer of (21). We apply the CG method on the normal equation

\[
\text{Re}[\mathbf{F}^*_\text{NDFT}(w \odot \mathbf{F}_{\text{NDFT}} f)] = \text{Re}[\mathbf{F}^*_\text{NDFT}(w \odot g)],
\]

**Algorithm 3:** CG inversion of the NDFT

**Input:** \( g = [g_{m,n}]_{m \in \mathcal{J}_M, n \in I_N} \in \mathbb{C}^{MN^{d-1}}, \ w \in \mathbb{R}_>^{MN^{d-1}}, \ f^{(0)} \in \mathbb{R}^{K^d}, \ J_{\text{CG}} \in \mathbb{N}. \)

\[ r^{(0)} := g; \]
\[ p^{(0)} := s^{(0)} := \text{Re}[\mathbf{F}^*_\text{NDFT}(w \odot r^{(0)})]; \]

for \( j = 0, 1, \ldots, J_{\text{CG}} \) do

\[
q^{(j)} := \mathbf{F}_{\text{NDFT}}p^{(j)}; \]
\[
\alpha_j := (s^{(j)*} s^{(j)}/(q^{(j)*} (w \odot q^{(j)})); \]
\[
f^{(j+1)} := f^{(j)} + \alpha_j p^{(j)}; \]
\[
r^{(j+1)} := r^{(j)} - \alpha_j q^{(j)}; \]
\[
s^{(j+1)} := \text{Re}[\mathbf{F}^*_\text{NDFT}(w \odot r^{(j+1)})]; \]
\[
\beta_j := (s^{(j+1)*} s^{(j+1)}/(s^{(j)*} s^{(j)})); \]
\[
p^{(j+1)} := s^{(j+1)} + \beta_j p^{(j+1)}; \]

end

**Output:** Approximate solution \( f^{(J_{\text{CG}})} \in \mathbb{R}^{K^d} \).
where $f$ is assumed to be real-valued. This approach results in Algorithm 3, which is known as CGNE (CG on the normal equations), CGNR (CG minimizing the norm of the residual) or CGLS (CG minimizing least squares). The iterative method requires the evaluation of $F_{\text{NDFT}}$ and $F_{\text{NDFT}}^*$ in each iteration. For a more detailed description of the algorithm, we refer to [36, 48].

Good weights $w$ ensure that $F_{\text{NDFT}}^*(w \odot g)$ is close to the desired solution $f$. In this case, the CG usually converges faster. One possibility to choose $w$ are the quadrature weights (20) with respect to $Y_{M,N}$ [48]. The CG algorithm is a simple regularization method, where the number of iterations acts as regularization parameter [21, Sect. 7].

### 5.3 Total variation regularization

In order to stabilize the inversion of the NDFT, we regularize (17) by the total variation (TV) semi-norm. For a discrete image $f \in \mathbb{R}^{K_d}$, the total variation becomes

$$TV(f) := \sum_{k \in \mathcal{I}_K^d} \|(\text{grad } f)_k\|_2 = \|\text{grad } f\|_{1,2},$$

see for instance Bredies & Lorenz [10], where the discrete gradient $\text{grad}: \mathbb{R}^{K_d} \to \mathbb{R}^{K_d \times d}$ yields a discrete vector field by applying the finite forward differences with respect to each axis. More precisely, the discrete gradient is defined by

$$(\text{grad } f)_k, \ell = (\hat{c}_\ell f)_k$$

with

$$(\hat{c}_\ell f)_k := \begin{cases} f_{k+e_\ell} - f_{k}, & k_\ell < \frac{K}{2} - 1, \\ 0, & k_\ell = \frac{K}{2} - 1, \end{cases}$$

(22)

for $k \in \mathcal{I}_K^d$ and $\ell \in \mathcal{J}_d$, where $e_\ell$ corresponds to the $\ell$th unit vector. The adjoint of the discrete gradient is the negative discrete divergence, i.e. $\text{grad}^* = - \text{div}$. Using finite backward differences, we define the discrete divergence by

$$\text{div } y := \sum_{\ell=1}^d \tilde{c}_\ell y, \ell$$

with

$$(\tilde{c}_\ell f)_k := \begin{cases} f_{k}, & k_\ell = -\frac{K}{2}, \\ f_{k} - f_{k-e_\ell}, & -\frac{K}{2} < k_\ell < \frac{K}{2} - 1, \\ -f_{k-e_\ell}, & k_\ell = \frac{K}{2} - 1, \end{cases}$$

where $y, \ell$ denotes the $\ell$th components of the discrete vector field $y \in \mathbb{R}^{K_d \times d}$.

The TV regularization is well known to promote cartoon-like images such as the objects we expect in our specific application. Besides this a priori information, we know that the images representing the physical object are real-valued and non-negative. Incorporating this knowledge, we propose to compute the NDFT by minimizing the variational formulation

$$\min_{f \in \mathbb{R}^{K_d}} \chi_{\mathbb{R}^{K_d}}(f) + \frac{1}{2} \|F_{\text{NDFT}}(f) - g\|_{2,w}^2 + \lambda \|\text{grad } f\|_{1,2},$$

(23)
where \( L := \text{grad} \) and \( \chi_{R^d_{\geq 0}} \) is the characteristic function over the non-negative orthant given by
\[
\chi_{R^d_{\geq 0}}(f) := \begin{cases} 
0, & \text{if } f_k \geq 0 \text{ for all } k \in I^d_K, \\
+\infty, & \text{otherwise}.
\end{cases}
\]

A convex minimization problem like (23) may be numerically solved with the primal-dual (PD) iteration by Chambolle & Pock [13], which consists in
\[
f^{(j+1)} := \text{prox}_{\tau F}(f^{(j)} - \tau(\nabla G(f^{(j)}) + L^*y^{(j)})),
\]
\[
y^{(j+1)} := \text{prox}_{\sigma H^*}(y^{(j)} + \sigma L(2f^{(j+1)} - f^{(j)}))
\]
for appropriate \( \tau, \sigma > 0 \). Here, \( \nabla G \) denotes the gradient of the differentiable function \( G \) in contrast to the discrete gradient (22) of a multidimensional signal. More generally, the proximal mapping of a convex function \( h : \mathbb{R}^K \to \mathbb{R} \cup \{-\infty, +\infty\} \) is defined by
\[
\text{prox}_h(x) := \arg \min_{y \in \mathbb{R}^K} h(y) + \frac{1}{2} \| x - y \|^2_2.
\] 

(24)

If \( h \) is additionally proper, i.e. not everywhere \( +\infty \) and never \( -\infty \), and lower semi-continuous, then the minimizer in (24) is unique, and the proximal mapping becomes single valued. Further, the Fenchel or convex conjugate of the convex function \( h \) is defined by
\[
h^*(x) := \sup_{y \in \mathbb{R}^K} \langle x, y \rangle - h(y).
\]

Since the proximal mapping of an indicator function is the projection to its support [4, Thm. 3.14], i.e.
\[
\text{prox}_{\chi_{R^d_{\geq 0}}}(x) = \text{proj}_{\chi_{R^d_{\geq 0}}}(x) := \arg \min_{y \in \mathbb{R}^d_{\geq 0}} \| x - y \|^2_2,
\]

for our specific formulation (23), the PD iteration becomes
\[
f^{(j+1)} := \text{proj}_{\chi_{R^d_{\geq 0}}}(f^{(j)} - \tau(\text{Re}[F^*_\text{NDFT}(w \odot (F_{\text{NDFT}}f^{(j)} - g))] - \text{div} y^{(j)})),
\]
\[
y^{(j+1)} := \text{prox}_{\sigma \| \cdot \|^2_{1,2}}(y^{(j)} + \sigma \text{grad}(2f^{(j+1)} - f^{(j)})).
\]

(25)

The remaining proximal mapping of the discrete TV semi-norm may be computed by exploiting
\[
\text{prox}_{\sigma \| \cdot \|^*_{1,2}}(y) = y - \sigma \text{prox}_{\| \cdot \|^2_{1,2}}(\frac{1}{\sigma} y),
\]

cf. [4, Thm. 14.3], and
\[
(\text{prox}_{\rho \| \cdot \|^*_{1,2}}(y))_{k,\ell} = \left(1 - \frac{\rho}{\max\{\|y_{k,\ell}\|_2, \rho\}}\right) y_{k,\ell}
\]
for some \( \rho > 0 \), see for example [15] and references therein.

The central pitfall of applying the PD iteration in practice is the selection of appropriate primal and dual step sizes \( \tau \) and \( \sigma \). In the literature, there exist several approaches to
Algorithm 4: PD inversion of the NDFT with TV

**Input:** \( g = F_{\text{NDFT}} f, w \in \mathbb{R}^{MN_d-1}, \lambda > 0, f^{(0)} \in \mathbb{R}^{K_d^d}, y^{(0)} \in \mathbb{R}^{K_d \times d}, \tau^{(0)} > 0, \sigma^{(0)} > 0, \rho = 0.005, c = 0.9, \beta = 1.5, \zeta = 0.25, J_{\text{PD}} \in \mathbb{N}. \)

**for** \( j = 0, 1, 2, \ldots, J_{\text{PD}} \) **do**

- Compute \( f^{(j+1)}, y^{(j+1)} \) by (25);
- Compute \( p^{(j+1)}, d^{(j+1)} \) by (26);
- Compute \( \alpha^{(j+1)}, \omega^{(j+1)}, \omega^{(j+1)} \) by (27);
- if \( \omega^{(j+1)} > c \) then \( \tau^{(j)} := \beta \tau^{(j)} \);
- if \( \omega^{(j+1)} < 0 \) then \( \tau^{(j)} := \zeta \tau^{(j)} \);
- if \( \omega^{(j+1)} > c \) then \( \sigma^{(j)} := \beta \sigma^{(j)} \);
- if \( \omega^{(j+1)} < 0 \) then \( \sigma^{(j)} := \zeta \sigma^{(j)} \);

Balancing: \( \tau^{(j+1)} := (\alpha^{(j+1)})^{\rho \tau^{(j)}}, \sigma^{(j+1)} := \sigma^{(j)} / (\alpha^{(j+1)})^{\rho} \);

**end**

**Output:** Approximate scattering potential \( f^{(J_{\text{PD}})} \).

Choose the step sizes adaptively [32, 63]. In our numerical experiments, we rely on the step size rules proposed in [63], which have been successfully applied to TV denoising in image processing. The main idea is to compute the primal and dual residuals

\[
\begin{align*}
    p^{(j+1)} := & \frac{1}{2} (f^{(j)} - f^{(j+1)}) - \text{Re}[F_{\text{NDFT}}^\ast w \odot F_{\text{NDFT}}(f^{(j)} - f^{(j+1)})] + \text{div}(y^{(j)} - y^{(j+1)}), \\
    d^{(j+1)} := & \frac{1}{2} (y^{(j)} - y^{(j+1)}) - \text{grad}(f^{(j)} - f^{(j+1)}),
\end{align*}
\]

where we added the residual with respect to the gradient \( \nabla G \). Further, we require the values

\[
\begin{align*}
    \alpha^{(j+1)} := & \frac{\|f^{(j+1)}\|_2}{\|y^{(j+1)}\|_2}, \\
    \omega^{(j+1)} := & \frac{\langle f^{(j)} - f^{(j+1)}, p^{(j+1)} \rangle}{\|f^{(j)} - f^{(j+1)}\|_2 \|p^{(j+1)}\|_2}, \\
    \omega^{(j+1)} := & \frac{\langle y^{(j)} - y^{(j+1)}, d^{(j+1)} \rangle}{\|y^{(j)} - y^{(j+1)}\|_2 \|d^{(j+1)}\|_2},
\end{align*}
\]

where the occurring inner products are defined via

\[
\begin{align*}
    \langle f, g \rangle := & \sum_{k \in I^d_K} f_k g_k \quad \text{and} \quad \langle y, z \rangle := \sum_{k \in I^d_K} \langle y_k, z_k \rangle.
\end{align*}
\]

Now, if \( f^{(j)} - f^{(j+1)} \) is aligned with primal residual \( p^{(j+1)} \), we increase the primal step size \( \tau \); and if \( f^{(j)} - f^{(j+1)} \) is opposed to \( p^{(j+1)} \), we decrease \( \tau \). We proceed analogously for the dual step size \( \sigma \). On the basis of the observation that a large \( \tau \) and a small \( \sigma \) decrease the primal residual at the cost of the dual residual [32], Yokata & Hontani [63] propose to balance both step sizes by multiplying \( \tau \) with a power of \( \alpha^{(j+1)} \) and dividing \( \sigma \) by the same power of \( \alpha^{(j+1)} \), which is greater than one if the primal residual dominates;
or less than one if the dual residual dominates. Summarized, we apply the PD iteration with the parameter updates in Algorithm 4, which we call the PD method (with TV) for ODT. A more detailed motivation behind the acceleration, backtracking and balancing of the step sizes may be found in [63].

5.4 Numerical backward transform

We numerically compare the three reconstruction approaches based on Algorithm 2, where the inverse NDFT step is realized via

i) the BP method (19),

ii) the CG method in Algorithm 3, and

iii) the PD method with TV in Algorithm 4.

Additionally, we apply TV denoising to the reconstructed images of i) and ii). The TV denoising (TVd) corresponds to finding a minimizer of

$$\min_{f \in \mathbb{R}^{K^d}} \chi_{\mathbb{R}^{K^d}}(\tilde{f}) + \frac{1}{2} \| \tilde{f} - f \|_2^2 + \lambda \| \text{grad } \tilde{f} \|_{1,2},$$

i.e., (23) with the identity instead of $F_{\text{NDFT}}$. In order to avoid the so-called “inverse crime,” we compute the data via a direct discretization of the convolution (3). For some of the tests, we also disturb the measurements by additive noise; so in this case we have only access to $D_{\text{tot}}^d f + \epsilon$ with $\epsilon \in \mathbb{C}^{MN^d-1}$ corresponding to the noise level $\| \epsilon \|_2 / \| D_{\text{tot}}^d f \|_2$.

All numerical tests were performed on a standard PC with an 8-core Intel Core i7-10700 and 32 GB memory using Matlab with the NFFT library [43]. Our code is available in the FourierODT toolbox.¹ We compare the reconstruction quality by means of the structural similarity index measure (SSIM) [61] and the peak signal-to-noise ratio

$$\text{PSNR}(f, g) := 10 \log_{10} \frac{\max_{k \in \mathbb{T}_K} |f_k|^2}{K^{-d} \sum_{k \in \mathbb{T}_K} |f_k - g_k|^2}, \quad f, g \in \mathbb{R}^{K^d}.$$  

Two-dimensional function. For a 2D simulation, we employ the discretization parameters $K = N = M = 240$ as well as $r_M = 40$ and $L_M = 60$. We choose $L_n = K/(4\sqrt{2}) \approx 42$, which ensures that $\mathcal{Y}_{M,N}$ is inside one periodicity interval of the NDFT. We fix the wave number $k_0 = 2\pi$, which means that all spatial measurements are in multiples of the wavelength of the incident field $u^{\text{inc}}$. The object rotates a full turn around the center. The object $f$ consists of different convex and concave shapes, see Figure 4a. The discrete sinogram $D_{\text{tot}}^d f$ and the Fourier space data approximating $F[f]$ on the set (13), which is contained in a disk of radius $\sqrt{2} k_0$, are shown in Figure 3.

¹https://github.com/michaelquellmalz/FourierODT
Table 1: Error for the reconstruction of the function of Figure 4a with exact data.

| Method        | PSNR   | SSIM   | Time (sec) |
|---------------|--------|--------|------------|
| BP            | 31.22  | 0.388  | 0.01       |
| BP & TVd      | 36.17  | 0.991  | 0.12       |
| CG            | 39.61  | 0.983  | 0.18       |
| CG & TVd      | 40.12  | 0.990  | 0.12       |
| PD            | 41.59  | 0.988  | 0.28       |

Figure 3: Visualization of the data and the respective Fourier space coverage.

Figure 4: Inversion of $D_{\text{tot}} f$ with 5% Gaussian noise using BP in (19), CG in Alg. 3, and PD with TV in Alg. 4. The BP and CG results are TV-denoised.
For the reconstructions, we use $J_{CG} = 20$ iterations for CG in Algorithm 3 and $J_{PD} = 50$ iterations for PD with TV in Algorithm 4. Note that the BP and the CG reconstruction only assume that $f$ is real-valued, whereas PD with TV incorporates the non-negativity of $f$. The reconstruction error for exact data and the computation times are shown in Table 1 (all reconstructions look very good and are visually almost indistinguishable). Figure 4 shows the reconstructions for 5% complex Gaussian noise. Different from above, the CG method is performed with $J_{CG} = 5$ iterations, which acts as regularization against the noise. The advantage of the TV regularization is clearly visible.

Instead of choosing an appropriate $\lambda$ for PD with TV by hand as in the above simulations, different choice strategies may be applied [21, Sect. 4]. We obtained promising results with the L-curve method [37], which does not require a priori knowledge of the noise level. This method consists of choosing $\lambda$ with respect to the “tip” of an L-shaped curve in a bilogarithmic plot of the residual $\|F_{NDFT}f_{\lambda} - g\|_{2,w}^2$ versus the regularization $\|\nabla f_{\lambda}\|_{1,2}$ for varying $\lambda$, where $f_{\lambda}$ denotes the reconstruction for a specific $\lambda$, and where $g$ is computed form the data $v_{m,ca}^*$. An exemplary L-curve is displayed in Figure 5, where we can spot the “tip” around $\lambda \approx 0.1$. A second, much weaker kink at the top left around $\lambda \approx 0.01$ can be easily ruled out as the corresponding reconstruction $f_{\lambda}$ looks very noisy.

**Three-dimensional function.** Our three-dimensional phantom contains a variety of shapes with smooth and non-smooth boundaries, see Figure 7a. The discretization parameters are the same as before. The object makes a full turn around the $x_2$ axis with the rotation angle $t \in [0, 2\pi]$. The measurements with respect to one illumination angle is shown in Figure 6. The respective Fourier space coverage $Y$ in (8) has the form of a horn torus and is depicted in Figure 6c, cf. [45]. The so-called missing cone around the $x_2$ axis in the Fourier space coverage makes the reconstruction more difficult and promotes certain artifacts, like horizontal stripes at the top and bottom in Figure 7.
Table 2: Error for the reconstruction of the function of Figure 7a with exact data.

|        | BP  | BP & TVd | CG  | CG & TVd | PD  |
|--------|-----|----------|-----|----------|-----|
| PSNR   | 29.07 | 32.79    | 33.36 | 33.82    | 34.36 |
| SSIM   | 0.614  | 0.987    | 0.955 | 0.988    | 0.957 |
| Time (sec) | 4    | 31       | 79   | 31       | 1395 |

Figure 6: Data $|u_{t}^{\text{tot}}(\cdot, r_{M})|$ for the function of Figure 7a at one fixed time step $t$ and the Fourier coverage $\mathcal{Y}$ in 3D.

Figure 7: Slice $x_{3} = 0.35$ of the 3D reconstruction from data with 5% Gaussian noise using BP in (19), CG in Alg. 3, and PD with TV in Alg. 4.
The errors for exact data and computation times are presented in Table 2. The reconstructions with noisy data are shown in Figure 7. The CG reconstruction is again of better quality than BP. Both, however, contain visible noise, which is compensated in the additional TV denoising performed afterwards, where we make $J_{\text{PD}} = 20$ iterations. Performing more iterations does not benefit the image quality significantly. The PD method with TV for the full inverse problem produces also a very good 3D reconstruction. However, the latter requires significantly more time since the primal-dual iteration converges rather slowly and requires $J_{\text{PD}} = 100$ iterations to obtain a satisfying result.

6 Phase retrieval in ODT

Different from the numerical experiments in Section 5.4, the phase of the complex diffraction patterns $u_{\text{tot}}^t$ is usually unknown in practice. In other words, only the intensity $|u_{\text{tot}}^t(\cdot, r_M)|$ is recorded. Due to the phase loss, the already ill-posed recovery problem is further hampered.

The numerical retrieval of an unknown phase traces back to the famous Gerchberg–Saxton algorithm [31], which was originally invented to capture a complex-valued object from its intensities in spatial and Fourier domain and was modified by Fienup [27] to recover an object from the modulus of its Fourier transform. The basic idea of Fienup’s error-reduction algorithm is to enforce known object constraints in object domain and known magnitude constraints given by the data in Fourier domain alternatingly. The error-reduction algorithm is a specific version of more general input-output algorithms, which may be read as Algorithm 5, where $D$ is a map modeling the measurement process, and where the sign function

$$\text{sgn}(z) := \begin{cases} \frac{z}{|z|}, & z \in \mathbb{C}\setminus\{0\}, \\ 1, & z = 0, \end{cases}$$

is applied element by element. The error-reduction algorithm and modifications of it are nowadays still well-established approaches to solve phase retrieval problems in practice.

For our specific application, the given data $d = |D(f)|$ corresponds to the measurement process modeled via $D_{\text{tot}}$ in (16). Since $D_{\text{tot}}$ is not invertible in general, we approximately compute $f^{(j)}$ via Algorithm 2. The object domain constraints of $f$ consist in the non-negativity and support constraint of the investigated physical object. Assuming that the support of $f$ is constrained in the ball of radius $r_s$, we may enforce them by setting

$$\tilde{f}_k^{(j)} := \begin{cases} \max\{f_k^{(j)}, 0\}, & \|x_k\|_2 \leq r_s, \\ 0, & \|x_k\|_2 > r_s, \end{cases}$$

(28) for $k \in I_k$. In the following, we refer to Algorithm 5 with the input rule $f^{(j+1/2)} := \tilde{f}^{(j)}$ as the error-reduction algorithm (for ODT).
Algorithm 5: General input-output algorithm

Input: \( d = |D(f)| \).

Initialize \( g^{(0)} := d \);

for \( j = 0, 1, 2, \ldots, J_{\text{IO}} \) do

\[
\begin{align*}
\textbf{Set } f^{(j)} := D^{-1}g^{(j)}, \text{ see Algorithm 2; } \\
\textbf{Set } f^{(j+1/2)} \text{ by applying object domain constraints on } f^{(j)} \text{ via (28) or (29); } \\
\textbf{Set } g^{(j+1/2)} := Df^{(j+1/2)}, \text{ see Algorithm 1; } \\
\textbf{Set } g^{(j+1)} := d \text{ sgn}(g^{(j+1/2)});
\end{align*}
\]

end

Output: Approximate scattering potential \( f^{(J_{\text{IO}})} \).

Instead of enforcing the object domain constraints strictly, the input of the next forward transform may be modified such that the output of the subsequent backward transform is pushed in direction of the feasible object signals. This procedure usually leads to a better numerical convergence of Algorithm 5. A typical choice of the next input \( f^{(j+1/2)} \) is known as the hybrid input-output (HIO) by Fienup [26]. For some fixed \( \beta \in (0, 1] \), the HIO step in Algorithm 5 consists of

\[
f^{(j+1/2)}_k := \begin{cases}
  f^{(j)}_k, & k \in \Gamma^{(j)}, \\
  f^{(j+1/2)}_k - \beta(f^{(j)}_k - \tilde{f}^{(j)}_k), & k \in I^d \setminus \Gamma^{(j)},
\end{cases}
\]

where \( \Gamma^{(j)} := \{ k \in I^d : f^{(j)}_k = \tilde{f}^{(j)}_k \} \) consists of all indices \( k \) where \( f^{(j)}_k \) satisfies the object domain constraints. The next input \( f^{(j+1/2)} \) is thus composed of the input \( f^{(j-1/2)} \) and output \( f^{(j)} \) of the last forward-backward transform. We henceforth refer to Algorithm 5 with input rule (29) as the HIO algorithm (for ODT).

The numerical performance of the error-reduction and the hybrid input-output algorithm may be increased by denoising the output of the forward-backward transform using the total variation. This idea has been successfully applied for example in Fourier and Fresnel diffraction imaging [28, 29]. If the inverse of the NDFT during the backward transform is computed by Algorithm 4, we automatically obtain a TV regularized output; so the backward transform corresponding to (23) goes hand in hand with the TV heuristic for the input-output phase retrieval methods.

7 Numerics of phase retrieval

In this section, we compare the performance of the CG method and the PD method in the context of phase retrieval in ODT, where we rely on the hybrid input-output algorithm in Section 6. In the second subsection, we compare our method with an existing one from literature, which only works well for a large distance \( r_M \) of the measurement plane.
We apply Algorithm 5 for the diffraction model $D^{\text{tot}}$. For the inversion of $D^{\text{tot}}$ required in each step of the input-output algorithm, we utilize either the CG method or the PD method with TV. We do now show the results with the BP method here, because it always performed worse than the CG. Since CG and PD are inside the loop of the input-output algorithm, the number of inner iterations can be reduced. In particular, the PD method in Algorithm 4 may be restarted in each step of the outer loop with the previous dual variable. Instead of restarting, the backtracking method may also be resumed, which significantly reduces the run time of the overall algorithm. Since the CG-based phase retrieval turns out to be much faster than the PD-based method, we utilize the CG phase reconstruction as starting point for phase retrieval with PD.

We employ the problem setting from Section 5.4. It is especially relevant for phase
retrieval that the images are padded with zeros to represent the support constraints (28). We impose the support constraint $r_s = 40$ in (28), which is larger than the actual support radius of the ground truth function of about 26. The results are shown in Figure 8, where the HIO is applied with the parameter $\beta = 0.7$. Especially for PD with TV, the result nearly coincide with the ground truth; so the missing phase does not decrease the image quality too much. With the CG method, there are some visible artifacts. However, executing more CG iterations may decrease the image quality because of the ill-posedness of the problem.

Adding 5% additive Gaussian noise to the intensity data $|D^{\text{tot}} f|$ does not decrease the reconstruction quality of HIO with TV-regularized PD inversion much, whereas the HIO reconstruction with CG becomes worse, see Figure 9. Raising the number of HIO iterations with CG results in even noisier reconstructions.

The L-curve method does not formally apply to this setting since the regularization parameter $\lambda$ appears only in the PD method and thus in the inner loop of Algorithm 5. However, we could still achieve some reasonable results, see Figure 10, where we plotted the residual $\|D^{\text{tot}} f - d\|_2$ versus the discrete TV semi-norm $\|f\|_{2,1}$. Note that there is a different behavior of the residual for very small and very large $\lambda$, where the HIO algorithm fails to find the right phase. However, these values may be excluded since no meaningful reconstruction occurs.

For the three-dimensional simulations, we impose the support constraint $r_s = 40$ in (28). The reconstructions are shown in Figure 11. There are some artifacts in the HIO/CG reconstruction. Raising the number of HIO iterations in this case promotes further noise artifacts, since the data have been computed using a discretization of the convolution (4). The slight differences between the data and reconstruction model avoids the inverse crime. The HIO method with PD and TV overcomes this issue and produces excellent reconstructions comparable to the known-phase inversion. Adding more noise to the data has a similar effect to the reconstruction as in the two-dimensional case, see Figure 12.
7.2 Wave propagation–backpropagation method

In contrast to applying a phase retrieval method to the full ODT model $D^{\text{tot}}$, an alternative approach proposed by Maleki & Devaney [52] takes into account the physical nature of diffraction tomography. We call it the MD approach. It is also based on the input-output methods of Section 6, but instead of solving the whole ODT problem in each step, only the wave propagation in free space is considered. In particular, we define the free space wave propagation operator $P$ for $v: \mathbb{R}^{d-1} \rightarrow \mathbb{C}$ by its Fourier transform

$$\mathcal{F}[Pv](\mathbf{y}') = e^{i\kappa(\mathbf{y}') r_M} \mathcal{F}[v](\mathbf{y}'), \quad \mathbf{y}' \in \mathbb{R}^{d-1},$$

where $\mathcal{F}$ denotes the $d-1$ dimensional Fourier transform. The inverse, the so-called free space backpropagation $P^{-1}$, applied to the field $u_i^{\text{ sca}}(\cdot, r_M)$ is assumed to approximately
match $u^{\text{sca}}_t(\cdot,0)$, which holds true for very thin samples. Then the support of

$$u^{\text{sca}}_t(\cdot,0) \approx \mathcal{P}^{-1}(u_t^{\text{tot}}(\cdot, r_M) - u^{\text{inc}}(\cdot, r_M))$$

is assumed to be contained in the ball of radius $r_s$.

Overall, the MD approach consists of two steps. First, we apply Algorithm 5 with $D$ replaced by $\mathcal{P} + e^{ik_0r_M}$ to the data $|u_t^{\text{tot}}(\cdot, r_M)|$ and impose that $u^{\text{sca}}_t(\cdot,0)$ has a compact support of radius $r_s$. In contrast to previous sections, we can assume neither the non-negativity nor the realness of $u^{\text{sca}}_t(\cdot,0)$. In the second step, we use an inversion method of Section 5 to recover $f$ using the retrieved phase of $u_t^{\text{tot}}$ from the first step.

As pointed out in [52], this method works only well if the distance $r_M$ of the measurement plane is very large, for instance $r_M > 1000$. To obtain decent reconstructions, we require larger measurement plane sizes $L_M$. Consequently $N$ has to become larger if the distance between neighboring grid points should stay the same as before.

For our numerical simulations, we chose $L_M = 240$ and $r_M = 1000$. Further, we raise the number of grid points to $N = 960$. The rest of the setting remains the same as in Section 7.1. The second step of the MD method is conducted with the inversion via PD with TV using $\lambda = 0.05$ and $J_{PD} = 100$. The results are shown in Figure 13. We see that the MD approach requires a very high number of iterations to find a good solution. Even 20 000 iterations are not sufficient, but 50 000 yield a reasonable reconstruction.

For a smaller distance $r_M$, even more iterations are necessary. With $r_M = 400$, we stopped after 5 million iterations, which took about 13 hours, and the reconstruction showed the right shape, but the level was still too low, see Figure 13d. In case of noisy data, we could not achieve a reasonable reconstruction with the MD approach.
8 Conclusion

We have compared reconstruction algorithms in ODT based on the Born approximation. For known-phase measurements, we compared the reconstruction based on three algorithms: the discrete backpropagation, the CG method, and the PD method with TV regularization. The backpropagation is the fastest, but the image quality was inferior compared to the others. The CG method was better and could still be improved when combined with TV denoising. In this case, the results are similar to the PD algorithm, which is usually the most accurate but also the slowest method.

For unknown phase, which causes the reconstruction problem to be more ill-posed, we achieved good results by applying the HIO algorithm, where the inner reconstruction is performed with the PD method. The image quality is comparable to the full phase inversion. The implementation with the CG method falls behind in terms of quality but, as it is much faster, gives good initial solutions for the HIO/PD method. By this procedure, the time requirements of PD are significantly reduced.

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