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A Markov chain model for predicting transient particle transport in enclosed environments

Chun Chen a, Wei Liu c, a, Chao-Hsin Lin b, Qingyan Chen a, c, *

a School of Mechanical Engineering, Purdue University, West Lafayette, IN, 47907, USA
b Environmental Control Systems, Boeing Commercial Airplanes, Everett, WA, 98203, USA
c Tianjin Key Laboratory of Indoor Air Environmental Quality Control, School of Environmental Science and Engineering, Tianjin University, Tianjin, 300072, China

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Obtaining information about particle dispersion in a room is crucial in reducing the risk of infectious disease transmission among occupants. This study developed a Markov chain model for quickly obtaining the information on the basis of a steady-state flow field calculated by computational fluid dynamics. When solving the particle transport equations, the Markov chain model does not require iterations in each time step, and thus it can significantly reduce the computing cost. This study used two sets of experimental data for transient particle transport to validate the model. In general, the trends in the particle concentration distributions predicted by the Markov chain model agreed reasonably well with the experimental data. This investigation also applied the model to the calculation of person-to-person particle transport in a ventilated room. The Markov chain model produced similar results to those of the Lagrangian and Eulerian models, while the speed of calculation increased by 8.0 and 6.3 times, respectively, in comparison to the latter two models.

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1. Introduction

In recent decades, outbreaks of airborne infectious diseases, including influenza [1], measles [2], tuberculosis [3], and severe acute respiratory syndrome (SARS) [4], have occurred indoors. All of these outbreaks have been proven to be associated with the airflow patterns in indoor environments [5]. An infected person can exhale particles carrying pathogens through the activities of breathing, coughing, talking, and sneezing, which are transient in nature. These particles can cause the transmission of infectious diseases to other occupants in the same enclosed environment [6,7]. Hence, it is essential to predict transient particle transport in the enclosed environment in order to improve air distribution design and reduce the risk of infection.

As a powerful airflow and contaminant modeling tool, computational fluid dynamics (CFD) has been widely used in predicting transient particle transport in enclosed environments. For particle modeling, the Eulerian and Lagrangian methods are popular. For instance, Li et al. [8], Seepana and Lai [9], and Chen et al. [10] studied the effects of ventilation parameters on person-to-person particle transport using an Eulerian drift flux model. Li et al. [11] and Chen et al. [12] investigated the effectiveness of covering a cough on reducing the receptor’s exposure using an Eulerian method. Hang et al. [13] used an Eulerian model to assess the influence of human walking on the transmission of airborne infectious diseases in a six-bed isolation room. Chen et al. [14], Gao et al. [15], and Zhang and Li [16] applied the RNG k-ε model with a Lagrangian method to calculate the transport of exhaled droplets in a dental clinic, an office, and a fully-occupied high-speed rail cabin. Zhang and Chen [17] compared the Eulerian and Lagrangian methods for predicting transient particle transport from a cough in a four-row aircraft cabin. Wang et al. [18] systematically compared the Eulerian and Lagrangian methods with various turbulence models and found that the Eulerian method was faster than the Lagrangian method. Both the Eulerian and Lagrangian methods can provide detailed information about transient particle concentration distributions. However, even with the Eulerian method, the unsteady-state calculation with iterations in each time step is considerably time-consuming. For instance, Wang et al. [18] reported that the computing times of the Eulerian and Lagrangian methods for calculating transient particle...
transport in a typical room were 62.2 and 84.9 h, respectively, on an eight-core cluster with two 2.5 GHz AMD quad-core processors.

Several studies have demonstrated the ability of the Markov chain technique to quickly predict spatial and temporal particle concentrations. For instance, Nicas [19] and Jones and Nicas [20,21] applied the Markov chain technique in a multi-zone model. However, this model does not inform users about particle movements between zones with respect to the required input values. Chen et al. [22] further used the CFD approach with Lagrangian particle tracking to obtain such information in order to complete the method. Since Lagrangian particle tracking is highly time-consuming, this method is suitable only for an extremely coarse grid. Therefore, a new model that not only works on a fine grid, as do the Eulerian and Lagrangian methods, but also runs faster than these two methods, is desirable. This investigation aimed to develop a Markov chain model for quickly predicting detailed transient particle concentration distributions in enclosed environments.

2. Methods

2.1. Airflow and turbulence model

This study used the renormalization group (RNG) k-ε model to calculate airflow and turbulence. This model has the best overall performance among all Reynolds-averaged Navier–Stokes (RANS) models for enclosed environments [23]. The equations for the RNG k-ε model can be found in the Fluent manual [24].

This investigation assumed that the airflow field was fixed. It could be problematic if the source was able to change the airflow pattern, as in the case of a powerful cough without covering the mouth. Therefore, this study assumed that the mouth was effectively covered when a person was coughing and that, as a result, the influence of the initial momentum from the cough on the receptor’s exposure was minimized [12]. Thus, the assumption of a fixed airflow field should be valid in most cases.

2.2. Markov chain model for transient particle transport

This study used the first-order homogenous Markov chain technique [25] to calculate transient particle transport. This Markov chain technique is effective for particles with a diameter smaller than 3 μm, which have negligible inertial effects [22]. Assuming that the CFD grid has n-1 cells, the additional cell n can be assigned to represent the space to which the particles are removed. Then the CFD grid has n-1 cells, the additional cell n can be assigned to represent the space to which the particles are removed. Then the transition probability matrix, pij:

\[ P = \begin{pmatrix} p_{11} & p_{12} & \cdots & p_{1n} \\ p_{21} & p_{22} & \cdots & p_{2n} \\ \vdots & \vdots & \ddots & \vdots \\ p_{n1} & p_{n2} & \cdots & p_{nn} \end{pmatrix} \quad (1) \]

where \( p_{ij} \) is the probability of a particle’s moving from cell i to cell j in a certain time step, \( \Delta t \). The transition probability matrix has the following property:

\[ \sum_{j=1}^{n} p_{ij} = 1, \quad p_{ij} \geq 0 \quad (2) \]

This property can be regarded as the constraint of mass balance for the whole domain. Since the movement of the particles normally does not have a major impact on the airflow field, the transition probability matrix is fixed.

The particle number vector at the present time (state k) is assumed to be:

\[ N_k = (N_{k1}, N_{k2}, \ldots, N_{kn}) \quad (3) \]

where \( N_{kj} \) represents the number of particles in cell i at time k. Then, after one time step (time \( k+1 \)), the number of particles in cell i can be calculated by:

\[ N_{k+1,i} = N_{ki}p_{i1} + N_{k,i}p_{i2} + \cdots + N_{kn}p_{in} \quad (4) \]

Thus, the particle number vector at time \( k+1 \) can be calculated by:

\[ N_{k+1} = N_kP \quad (5) \]

If one calculates the particle transport from time zero, the particle number vector at time k can be calculated by:

\[ N_k = N_{init}P^k \quad (6) \]

where \( N_{init} \) is the initial particle number vector. The particle number concentration in cell i at time k can be calculated by:

\[ C_{ki} = \frac{N_{ki}}{V_i} \quad (7) \]

where \( V_i \) is the volume of the cell.

The transition probability matrix can require a considerably large storage memory for a normal CFD grid. To reduce the size of the matrix, Eq. (4) was rewritten as:

\[ N_{k+1,i} = N_{ki}p_{i1} + \sum_{nb} N_{k,nb}p_{nb,i} \quad (8) \]

where the subscript nb represents the neighboring cells or boundaries. Eq. (8) shows that the Markov chain model does not require iterations in each time step. Therefore, this model has the potential to reduce the computing cost.

2.3. Transition probabilities

The key operation in applying the Markov chain technique to the calculation of transient particle transport is to obtain the transition probabilities, \( p_{ij} \). Again, \( p_{ij} \) is the probability of a particle’s moving from cell i to cell j in a certain time step, \( \Delta t \). The first step is to calculate the probability of a particle’s remaining in the current cell in \( \Delta t \), \( p_{ii} \). It is assumed that there are \( N_0 \) particles present in cell i at time zero and that these particles can be removed only by the flow of air. The particle mass balance equation for this cell is [19]:

\[ \frac{dN_i(t)}{dt} = \frac{N_i(t)}{V_i} \sum_{nb} Q_{inb} \quad (9) \]

where \( Q_{inb} \) is the airflow rate from cell i to the neighboring cell. Solving Eq. (9) leads to the following equation [19]:

\[ N(\Delta t) = N_0 \exp \left( -\sum_{nb} \frac{Q_{inb}}{V_i} \Delta t \right) \quad (10) \]

Therefore, after a certain time step, \( \Delta t \), \( N(\Delta t) \) particles remain in this cell. Thus, the probability of a particle’s remaining in the current cell in \( \Delta t \) can be expressed as [19]:

\[ p_{ii} = \exp \left( -\sum_{nb} \frac{Q_{inb}}{V_i} \Delta t \right) \quad (11) \]
If cell \( j \) is one of the neighboring cells, the probability of a particle's moving from cell \( i \) to cell \( j \) in \( \Delta t \) can be calculated by Ref. [19]:

\[
p_{ij} = \frac{Q_{ij}}{\sum_{nb} Q_{inb}} (1 - p_{ii})
\]

(12)

where \( Q_{inb} \) consists of the mean airflow rate \( (Q_{\text{mean},i,nb}) \) and the turbulent fluctuating airflow rate \( (Q_{\text{fluctuating},i,nb}) \) from cell \( i \) to the neighboring cell:

\[
Q_{inb} = Q_{\text{mean},i,nb} + Q_{\text{fluctuating},i,nb}
\]

(13)

The mean airflow rate from cell \( i \) to the neighboring cell can be obtained from the CFD simulation results. The turbulent fluctuating airflow rate from cell \( i \) to the neighboring cell is determined on the basis of the discrete random walk (DRW) model [26]. The turbulent fluctuating velocity in cell \( i \) can be calculated by:

\[
v'_i = \xi \sqrt{2k_i/3}
\]

(14)

where \( \xi \) is a standard normal random number and \( k_i \) is the turbulent kinetic energy in cell \( i \). This study estimated the turbulent fluctuating airflow rate from cell \( i \) to the neighboring cell as:

\[
Q_{\text{fluctuating},i,nb} = \alpha_{i,nb} \sqrt{2k_i/3} \cdot A_{i,nb}
\]

(15)

where \( A_{i,nb} \) is the area of the connecting face between cell \( i \) and the neighboring cell. The coefficient \( \alpha_{i,nb} \) is calculated by:

\[
\alpha_{i,nb} = 2 \left( 1 - \phi \left( \frac{\Delta s_{i,nb} / \Delta t}{\sqrt{2k_i/3}} \right) \right)
\]

(16)

where \( \Delta s_{i,nb} \) is the distance between the centroid of cell \( i \) and that of the neighboring cell. The function \( \Phi() \) is the cumulative distribution function for a standard normal distribution:

\[
\Phi(x) = \frac{1}{2} \left( 1 + \text{erf} \left( \frac{x}{\sqrt{2}} \right) \right)
\]

(17)

where \( \text{erf}() \) is the error function. The coefficient \( \alpha_{i,nb} \) considers the effects of the distance between the cell centroids and the time step size on the turbulent dispersion of particles. For instance, when the distance between the cell centroids, \( \Delta s_{i,nb} \), is extremely small, its effect is negligible, and the coefficient \( \alpha_{i,nb} \) should be equal to 1. However, when the distance between the cell centroids is extremely large, a particle originally at the center of the cell has almost no chance of moving to the neighboring cell in one time step, and the coefficient should be equal to 0.

This investigation used the CFD code ANSYS Fluent 12.1 [26] to calculate the airflow field. A user-defined function (UDF) was implemented in order to realize the Markov chain model.

3. Validation

This investigation used two cases, transient particle transport in an isothermal ventilated chamber [27] and a chamber with displacement ventilation [28], to validate the Markov chain model. This section discusses the validation results.

3.1. Particle transport in an isothermal ventilated chamber

The first study was the case of transient particle transport in an isothermal ventilated chamber as addressed by Zhang et al. [27]. Fig. 1 shows the configuration of the chamber with spatial dimensions of 4 m in length, 2.1 m in width, and 2.4 m in height. The size of both the supply inlet and exhaust was 0.3 m × 0.3 m. The supply inlet was located 0.3 m from the ceiling, while the exhaust was located 0.3 m from the floor. The averaged supply-air velocity magnitude and turbulence intensity were 0.84 m/s and 20%, respectively. The incident angle of the supply air was 10° downward. Particles with a size of 1 μm were injected through the inlet into the chamber. Transient particle concentrations were measured at two locations on a vertical line in the z-directional center-cutting plane and 1 m away from the inlet. The measurement locations were 0.9 and 1.8 m from the floor. Two optical particle counters were used to measure the transient particle concentrations at the inlet and one of the measurement locations simultaneously. Therefore, the experiment was conducted twice in order to obtain the results at the two locations.

Note that the current Markov chain model can only calculate transient particle transport from a pulse source. However, the measurement results show that there was an initial peak in the particle concentration, and then the concentration decreased significantly to a stable level. Thus, this study first divided the inlet concentration into various pulse sources with duration of one time step \( \Delta t \). The Markov chain model was then used to calculate the transient particle concentrations from a pulse source, \( \text{C}_{\text{MC}} \), with an inlet particle number concentration of 1 per m³. The total particle concentration can be calculated using the superimposition method [29]:

\[
C(t) = C(m \cdot \Delta t) = \sum_{n=0}^{m} C_{\text{in}}(n \cdot \Delta t) \cdot C_{\text{MC}}(m - n + 1) \cdot \Delta t
\]

(18)

where \( \Delta t \) is the time step size, \( m \) is the number of calculation steps, \( C_{\text{in}}(n \cdot \Delta t) \) is the inlet particle concentration at time \( n \Delta t \), and \( C_{\text{MC}}(m - n + 1) \cdot \Delta t \) is the particle concentration from a pulse source with an inlet particle number concentration of 1 per m³ at time \( (m - n + 1) \cdot \Delta t \).

Three grid resolutions (4,934, 18,009, and 134,090) were tested for CFD grid independence. The resolution of 18,009 was sufficiently fine to capture the turbulent flow in the chamber. The time step size was set at 0.01 s. The independence test showed that this time step size was sufficiently fine to capture the transient features.
Particle deposition and resuspension are negligible at a particle size of 1 μm [30,31]. Fig. 2 compares the numerical results for transient particle concentration with the experimental data. Note that two sets of simulations were performed on the basis of the corresponding inlet particle concentrations, as shown in Fig. 5 of Zhang et al. [27]. In Fig. 2(a), both the Markov chain model and the experimental data exhibit an initial peak in particle concentration. In Fig. 2(b), the model and the experimental data both display smaller peaks in particle concentration than those in Fig. 2(a). Furthermore, the Markov chain model can capture the fact that the peak at this location was delayed in time. In general, the trends in transient particle transport predicted by the Markov chain model agree well with the experimental data.

3.2. Particle transport in a chamber with displacement ventilation

The second case was a chamber with displacement ventilation, as shown in Fig. 3 and used by Bolster and Linden [28] for measuring transient particle transport. The chamber had dimensions of 2.6 m in length, 1.3 m in width, and 1.8 m in height. The air was supplied through four linear slot diffusers, each with a width of 2.5 cm, that were installed at the edges of the floor. The exhausts were located at ceiling level according to the schematic in Fig. 1 of Bolster and Linden [28]. A heated box with a power of 65 W was located at the center of the floor. The box had dimensions of 0.2 m in length, 0.2 m in width, and 0.22 m in height. The supply-air velocity was 0.08 m/s. Particles with a size of 2 μm were injected from a point above the heated box for 328 s. Transient particle concentrations were measured at five locations on a vertical line in the x-directional center-cutting plane and 0.65 m away from the heated box. The measurement locations were 0.2, 0.6, 1.1, 1.4, and 1.7 m from the floor.

This study first used the Markov chain model to calculate C_{MC} and then applied the superimposition method (Eq. (18)) to calculate the total particle concentration. This investigation tested three grid resolutions (19,100, 53,740, and 383,120) for CFD grid independence. The resolution of 53,740 was sufficiently fine to capture the turbulent flow in the chamber. The time step size was set at 0.01 s. The independence test showed that this time step size was sufficiently fine to capture the transient features. Particle deposition and resuspension at a particle size of 2 μm were neglected [30,31]. Fig. 4 compares the numerical results for transient particle concentration with the experimental data. All the particle concentrations were normalized by the concentration at the source. The Markov chain model and experimental data display similar particle concentration profiles at the locations with heights of 1.7 and 1.4 m. At the location with a height of 1.1 m, the peak in the particle concentration was delayed in comparison with the peaks at the 1.7 and 1.4 m locations, and this delay was correctly captured by the Markov chain model. Furthermore, the model correctly predicted much lower particle concentrations (almost zero) at the location with a height of 0.2 and 0.6 m than at the other locations. To keep this paper concise, the results at these two locations are not presented here. Generally speaking, the trends in the normalized particle concentration distributions predicted by the Markov chain model again agreed reasonably well with the experimental data.

4. Simulation of person-to-person particle transport in a ventilated room

This study used the validated Markov chain model to predict person-to-person particle transport in a ventilated room. This
section discusses the performance of the Markov chain model in a real-life application.

4.1. Case description

This case was person-to-person particle transport in a ventilated room, as shown in Fig. 5 and studied by Chen et al. [12]. Two persons, represented by heated manikins, were seated face to face in the room, with a distance of about 1.0 m between their noses. The person on the left was assumed to be the index person, while the one on the right was the receptor. The room was ventilated by a mixing ventilation system with an air change rate of 3 ACH. The forced air and thermal plumes generated by the heated manikins formed a mixed convection airflow pattern. The index person was assumed to have a release of particles with zero velocity at time zero. The particle release duration was 0.15 s. A particle size of 1 μm was assumed in order to represent fine particles. Obviously, this case is more complicated than the previously discussed validation cases because of the complicated manikin geometry with unstructured tetrahedral grids. This study used the case to further assess the performance of the Markov chain model in a realistic scenario.

4.2. Simulation results

Since no experimental data was available for this case, this study used the Lagrangian and Eulerian models as benchmarks to assess the performance of the Markov chain model. This investigation used a grid resolution of 1,446,790 in the simulation, which was sufficient to capture the turbulent flow in the room [12]. The evaporative process is almost instantaneous for droplets with a diameter of 1 μm [32]. The time step size was 0.1 s. The independence test showed that this time step size was sufficient to capture the transient features. The calculations for this case were performed over a time period of 5 room time constants. For the Lagrangian model, the particle number injected from the source was $2.29 \times 10^6$, which was calculated using the method proposed by Chen et al. [33].

Fig. 6 compares the time-varying particle concentration distributions predicted by the Markov chain model with those predicted by the Lagrangian and Eulerian models in the first 100 s. All three models show that the exhaled particles initially moved upward.
with the thermal plume generated by the index person. The particles then dispersed throughout the room and reached the receptor. It can be seen in Fig. 6 that the Markov chain and Lagrangian models both predicted slower particle dispersion than did the Eulerian model. Note that both the Markov chain and Lagrangian models use the principle of the random walk model (Eq. (14)) to calculate the turbulent diffusion, while the Eulerian model includes the turbulent diffusion term in the particle governing equation. The numerical diffusion introduced by the Eulerian model may be an important reason for its more dispersive characteristics. Generally speaking, the trends in transient particle transport predicted by the Markov chain model agree well with both the Lagrangian and Eulerian models. For the calculation as a whole in this case, the Markov chain model was 8.0 times faster than the Lagrangian model and 6.3 times faster than the Eulerian model.

5. Discussion

There are a number of limitations to the present study, beginning with the assumption of a steady-state airflow field. For instance, some sources could change the airflow pattern, such as a powerful cough or sneeze from an uncovered mouth. In these cases, the probability transition matrix would also change. Therefore, the Markov chain model developed in this study is suitable only for those scenarios in which the mouth is effectively covered or the influence of the exhaled air is negligible. In the future, we intend to develop an improved Markov chain model for transient particle transport under unsteady-state airflow conditions. Note that, when combining with the superimposition method, the Markov chain model can also be used for predicting steady-state particle concentrations with a continuous source. However, when compared with the steady-state Eulerian model, the Markov chain model is more time-consuming because it needs to be performed under a transient condition. Therefore, the Markov chain model is not superior for steady-state particle concentration predictions.

The Markov chain model that was developed considers the dispersion of particles by the mechanisms of advection and turbulence diffusion. For particles with a diameter smaller than 3 μm, as were used in this study, these are the only important mechanisms in typical indoor environments [30]. If only these two mechanisms are considered, this model can also be used for tracer gas simulations. However, for particle transport, there are other mechanisms, such as gravitational settling, thermophoresis, particle fluctuation due to turbulence, and particle acceleration. Zhao et al. [30] indicated that gravitational settling could significantly affect the particle concentration distribution for particles with a diameter larger than 5 μm. Thus, to model the transient transport of coarse particles, the effect of gravitational settling should be further considered. Furthermore, for coarse and ultrafine particles in a room with a low air change rate, the influence of particle deposition on the particle concentration distribution may be considerable. Therefore, the implementation of particle deposition into the current Markov chain model deserves further study.

6. Conclusions

This investigation developed a Markov chain model for quickly predicting transient particle transport in enclosed environments. Within the scope of this research, the following conclusions can be drawn:

(1) The proposed Markov chain model can be used for predicting detailed information about transient particle transport in enclosed environments.

(2) The Markov chain model increased the speed of calculation by 8.0 and 6.3 times in comparison with the Lagrangian and Eulerian models, respectively, for the case that was studied.

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References

[1] Moser MR, Bender TR, Margolis HS, Noble GR, Kendal AP, Ritter DG. An outbreak of influenza aboard a commercial airliner. Am J Epi 1979;110:1–6.
[2] Bloch AB, Orenstein WA, Ewing WM, Spain WH, Mallison GF, Herrmann KL, et al. Measles outbreak in a pediatric practice: airborne transmission in an office setting. Pediatrics 1985;75:676–83.
[3] Menzies D, Fanning A, Yuan L, FitzGerald JM. Hospital ventilation and risk for tuberculous infection in Canadian health care workers. Ann Int Med 2000;133:779–89.
[4] Olsen SJ, Chang H, Cheung TY, Tang AF, Fisk TL, Ooi SP, et al. Transmission of the severe acute respiratory syndrome on aircraft. New Eng J Med 2003;349:2416–22.
[5] Li Y, Leung GM, Tang JW, Yang X, Chao C, Lin JL, et al. Role of ventilation in airborne transmission of infectious agents in the built environment—a multidisciplinary systematic review. Indoor Air 2007;17:2–18.
[6] Nicas M, Nazaroff WW, Hubbard A. Toward understanding the risk of secondary airborne infection: emission of respirable pathogens. J Occup Environ Hyg 2005;2:143–54.
[7] Morawska L. Droplet fate in indoor environments, or can we prevent the spread of infection? Indoor Air 2006;16:335–47.
[8] Li X, Niu J, Gao N. Spatial distribution of human respiratory droplet residuals and exposure risk for the co-occupant under different ventilation methods. HVAC&R Res 2011;17:432–45.
[9] Seepana S, Lai ACK. Experimental and numerical investigation of interpersonal exposure of sneezing in full-scale chamber. Aerosol Sci Tech 2012;46:485–93.
[10] Chen C, Zhu J, Qu Z, Lin C-H, Jiang Z, Chen Q. Systematic study of person-to-person contaminant transport in mechanically ventilated spaces (RP-1458). HVAC&R Res 2014;20:80–91.
[11] Li X, Niu J, Gao N. Co-occupant’s exposure of expiratory droplets—Effects of mouth coverings. HVAC&R Res 2012;18:575–87.
[12] Chen C, Lin C-H, Jiang Z, Chen Q. Simplified models for exhaled airflow from a cough with the mouth covered. Indoor Air 2014;24:580–91.
[13] Zhang N, Zheng Z, Eckels S, Nadella VB, Sun X. Transient response of particle transport in enclosed environment. Build Environ 2012;47:40–52.
[14] Chen C, Zhao B, Cui W, Dong L, An N, Ouyang X. The effectiveness of an air cleaner in controlling droplet/aerosol particle dispersion emitted from a patient’s mouth in the indoor environment of dental clinics. J R Soc Interface 2010;7:1105–18.
[15] Gao N, He Q, Niu J. Numerical study of the lock-up phenomenon of human exhaled droplets under a displacement ventilated room. Build Simul 2012;5:51–60.
[16] Zhang L, Li Y. Dispersion of coughed droplets in a fully-occupied high-speed rail cabin. Build Environ 2012;47:58–66.
[17] Zhang Z, Chen Q. Comparison of the Eulerian and Lagrangian methods for predicting particle transport in enclosed spaces. Atmos Environ 2007;41:5236–48.
[18] Wang M, Lin C-H, Chen Q. Advanced turbulence models for predicting particle transport in enclosed environment. Build Environ 2012;47:40–9.
[19] Nicas M. Markov modeling of contaminant concentrations in indoor air. AIHAJ 2000;61:484–91.
[20] Jones RM, Nicas M. Benchmarking of a Markov multizone model of contaminant transport. Ann Occup Hyg 2014;58:1018–31.
[21] Jones RM, Nicas M. Experimental evaluation of a Markov multizone model of particulate contaminant transport. Ann Occup Hyg 2014;58:1032–45.
[22] Chen C, Lin C-H, Long Z, Chen Q. Predicting transient particle transport in enclosed environments with the combined computational fluid dynamics and Markov chain method. Indoor Air 2014;24:81–92.
[23] Zhang Z, Zhai ZQ, Zhang W, Chen Q. Evaluation of various turbulence models in predicting airflow and turbulence in enclosed environments by CFD: part 2; comparison with experimental data from literature. HVAC&R Res 2007;13:871–86.
[24] Coudhury D. Introduction to the renormalization group method and turbulence modeling. Canonsburg: Fluent Inc; 1993. Technical Memorandum TM-107.
[25] Ross SM. Stochastic processes. 2nd ed. John Wiley & Sons, Inc; 1996.
[26] ANSYS. Fluent 12.1 documentation. Lebanon, NH: Fluent Inc.; 2010.
[27] Zhang N, Zheng Z, Eckels S, Nadella VB, Sun X. Transient response of particle distribution in a chamber to transient particle injection. Part. Part. Syst Charact 2009;26:199–209.
[28] Bolster DT, Linden PF. Particle transport in low-energy ventilation systems. Part 2: transients and experiments. Indoor Air 2009;19:130–44.
[29] Gupta JK, Lin C-H, Chen Q. Inhalation of expiratory droplets in aircraft cabins. Indoor Air 2011;21:341–50.
[30] Zhao B, Chen C, Tan Z. Modeling of ultrafine particle dispersion in indoor environments with an improved drift flux model. J Aerosol Sci 2009;40:29–43.
[31] Zhu Y, Zhao B, Zhou B, Tan Z. A particle resuspension model in ventilation ducts. Aerosol Sci Technol 2012;46:222–35.
[32] Chen C, Zhao B. Some questions on dispersion of human exhaled droplets in ventilation room: answers from numerical investigation. Indoor Air 2010;20:95–111.
[33] Chen C, Liu W, Lin C-H, Chen Q. Accelerating the Lagrangian method for modeling transient particle transport in indoor environments. Aerosol Sci Tech 2015. http://dx.doi.org/10.1080/02776882.2015.1031724.