Recent advances in hybrid measurement methods based on atomic force microscopy and surface sensitive measurement techniques

Stephan Handschuh-Wang, Tao Wang and Xuechang Zhou

AFM was proposed in the 1990s as a tool to determine the topography at a sub-micrometer level. Since then AFM proved to be a valuable tool in material science and physical chemistry. Soon after successful application of AFM, it was employed for biological applications. The success of AFM can be ascribed to the high sensitivity, versatility, and resolution (1000 times higher resolution compared to optical microscopy). However, it intrinsically lacks amongst others chemical sensitivity. These limitations of AFM can be overcome by coupling it to orthogonal (complementary) optical (i.e. microscopy techniques) or non-optical techniques (i.e. Kelvin method). Such combinations are capable to garner information on morphological and mechanical properties of a sample together with fluorescence, spectroscopic (IR/Raman/fluorescence), electric, temperature or conductivity. Recently, advances in microscopy and super-resolution techniques enable the collection of even more than 2 measurands. Furthermore, new combinations, such as the photothermal-induced resonance (PTIR), a combination of IR spectroscopy and AFM, and scanning near-field ellipsometry microscopy (SNEM), a combination of ellipsometry and AFM, are actively researched, widening the adoptability of orthogonal combinations relying on AFM, while researchers devote tremendous effort to enhance established hybrid methods, such as tip-enhanced Raman spectroscopy (TERS). Here, we introduce hybrid measurement techniques, relying on AFM and complementary techniques. The main focus of these hybrid techniques is on the combination with optical techniques as there has been much progress in the past few years and we can contribute our expertise in this field. For each combination, the working principle is explained briefly and applications of such combinations are pointed out. Finally, a short comprehension is given with basic...

Stephan Handschuh-Wang obtained his Diploma degree in physical chemistry from the University of Technology Dortmund in 2010. He pursued his PhD with Professor Holger Schönherr at the University of Siegen on the study of soft matter interfaces and obtained his PhD in 2016. Dr Handschuh-Wang is currently a postdoctoral fellow of Prof. Xuechang Zhou’s group at Shenzhen University. His previous and current research interests are focused on phenomena at the interface of preferably soft matter, in particular, the characterization and application of novel functional interfaces.

Tao Wang obtained her bachelor and master degree in material science and engineering from the Dalian University of Technology in 2011. She pursued her PhD with Professor Xin Jiang at the University of Siegen on the study of surface science and technology and obtained her PhD in 2015. Dr Tao Wang is currently a postdoctoral fellow of Prof. Yongbing Tang’s group at Shenzhen Institutes of Advanced Technology, Chinese Academy of Sciences. Her previous and current research interests are focused on surface coating, surface functionalization and interactions of molecules in applications of mechanical engineering, materials science, and biomedicine.
1. Introduction

Advances in science are closely related to advances in the design and construction of analysis tools. Here, confocal laser scanning microscopy should be mentioned with its unprecedented high lateral resolution and optical slicing ability. A second measurement technique, which made further advances possible, was atomic force microscopy. The atomic force microscope (AFM) rapidly emerged as an invaluable tool for direct measurement of topography and intermolecular forces with atomic resolution for a broad spectrum of applications, such as electronics, semiconductors, materials and manufacturing, polymers, biology, and biomaterials. An AFM is able to measure a sample at ambient conditions and even in liquid or buffer solutions, which is in contrast to scanning tunneling microscopy (STM), scanning electron microscopy (SEM) and transmission electron microscopy (TEM). This feature renders AFM especially useful for in vitro measurements of biological samples. Furthermore, AFM can employ several operation modes, which yields additional capabilities and makes it a powerful tool for several applications. These operation modes are for example contact mode, intermittent mode (topography), lateral force microscopy (friction) and noncontact mode, force modulation (elasticity) and phase imaging (dissipation). Nanoindentation can be utilized to determine in situ the mechanical properties of specific points and areas of a sample without change of the cantilever, tip, measurement equipment, and sample. A widespread technique is force modulation microscopy (FMM), which is utilized to characterize mechanical properties of polymers or composite material to detect inhomogeneities or contaminations. In biological regime, AFM can be utilized to determine biomechanical properties, changes in mechanical properties of cells, membranes and other biomaterials. AFM can be utilized to determine the adhesion of the tip and the surface. By functionalizing the tip with different probes, such as nanoparticles or molecules, interaction forces between two surfaces, a surface and a biological molecule or two biological molecules (single molecule force spectroscopy (SMFS)) can be determined. AFM is utilized in a wide range of disciplines in natural sciences, including solid state physics (e.g. identification of atoms at surfaces, sensor of electric charge and dynamic lateral friction microscopy), semiconductor science (e.g. topography, conductivity and current sensing), molecular engineering (e.g. nano-manipulation), polymer chemistry (e.g. surface structure, chemical sensing and viscoelasticity), surface chemistry (e.g. roughness, height, friction and surface rheology), molecular biology (e.g. DNA and chromosome studies and monitoring biological processes), cell biology (cell imaging & mechanical properties) and medicine (e.g. virology and tissue/organ imaging). Besides, new operation modes for the AFM are actively developed, such as scanning probe lithography and non-contact mode, and nowadays multiparametric AFM imaging is possible, further diversifying the field of application.

However, AFM as a stand-alone technique retains a few limitations. Identification of the surface termination or chemical composition of a sample is beyond its reach, as AFM is an indirect measurement technique it intrinsically lacks chemical information. Furthermore, AFM resembles a technique relying on the analysis of a surface by a probing stick (cantilever), without seeing the morphology directly. This often results in challenging and time-consuming search for a specific region of interest (ROI), similar to finding the light-switch in a dark room. Hence, many novel AFMs are equipped with a camera, facilitating laser alignment and ROI identification. Yet, the camera is typically only capable of ascertaining a rough knowledge of the surface (mm range), whereas the AFM measures in μm and nm range. Therefore, combining AFM with optical microscopy, confocal laser scanning microscopy or super-resolution techniques provide an advantage over stand-alone AFM techniques.

A combination of AFM and an orthogonal optical measurement technique, such as confocal laser scanning microscopy (CLSM), Raman (tip-enhanced Raman spectroscopy (TERS)) or infrared (photothermal-induced resonance (PTIR)), or non-optical techniques, like scanning thermal force microscopy, makes it possible to detect chemical information, identify the chemical composition or detect the thermal conductivity at high (lateral) resolution, which also offers new information on resolution and field of application of all major combinations. We envision that this review is helpful to those confronted with combined measurements for the first time, for experienced researchers, needing quick access to recent literature as it may convey new ideas for problems in analysis, as well as for researchers, who develop novel combined methods.
opportunities to gather multidimensional data from a given system. In combinations of an optical technique with AFM, both techniques retain their individual capabilities, which means the resolution and the information garnered by a method stays the same (obviously, the case for CLSM) or is in some cases improved (for tip-enhanced methods, such as TERS and PTIR). Furthermore, new capabilities arising from the versatility of the AFM can expand the capability of a combined setup. For example, an AFM-CLSM combination can make use of fluorescence modulation effects, which arise from the AFM tip in the vicinity of fluorescent molecules. These effects can either be enhancement or quenching of fluorescence, leading to a change in the excited state lifetime and can be utilized to enhance the spatial resolution of the CLSM/FLIM (fluorescence lifetime imaging microscopy).

Tremendous effort is concentrated on the implementation of non-optical methods, such as Kelvin probe thermal microscopy into the AFM. These combined methods allow concomitant measurement of topography with a localized surface potential, thermal information or thermal conductivity, which is important for material science and engineering, for example, mapping of semiconductors and their work functions.

This review covers the combination of optical and non-optical surface sensitive techniques with the AFM. An overview of the hybrid methods discussed in this article is given in Fig. 1. For comparison, firstly, super-resolution techniques are introduced, which are capable of resolving the resolution of optical images, with its advantages and drawbacks. Subsequently, the main focus is on combinations of optical methods, especially fluorescence microscopy, and CLSM, as with these examples the alignment, an important issue for hybrid methods, can be introduced easily. Afterwards, combinatorial methods based on AFM-CLSM are introduced, such as the combination of AFM with FLIM and stimulated emission depletion microscopy (STED), which are viable and recently developed candidates for predominantly addressing biological samples. Important representatives beside fluorescence-based methods are introduced hereafter, for example combination of AFM with Raman, tip-enhanced Raman scattering (TERS), and infrared spectroscopy, photothermal-induced resonance (PTIR). Thereafter, combinations of AFM with non-optical methods are introduced, such as the combination of AFM with Kelvin’s method (a method for determining the contact potential difference), Kelvin probe force microscopy (KPFM), and with thermal conductivity measurement, scanning thermal microscopy (SThM). Examples out of scientific publications illustrate the applicability of these orthogonal measurement techniques and their scope. Finally, the advantages and disadvantages of these techniques are evaluated and the recent progress of hybrid methods relying on AFM is assessed.

As this review article focuses on the recent advances of hybrid methods and novel hybrid methods since 2009, this article cannot cover the basic principle of the AFM and its different measurement modes. The interested reader is referred to the well-established literature regarding AFM, for example the books by Eaton, West: Atomic force microscopy for a more theoretic overview and Schönherr, Vancso: Scanning Force Microscopy of Polymers for a more practical introduction and the recent inspiring reviews by Zhong and Yan (AFM for nanomaterial research), Allison et al. (AFM for biological samples) and Dufrêne et al. (imaging modes, AFM for molecular and cell biology).

2. Combination of AFM with optical surface sensitive methods

Well-established methods in biology and nanotechnology, i.e. for cell-imaging or imaging of nanoparticles, are fluorescence microscopy and confocal fluorescence microscopy or confocal laser scanning microscopy (CLSM). CSLM was first patented in 1957 by Marvin Minsky. Its impact for research applications arises from the drastic improvement of optical resolutions to an unprecedented level of up to 180 nm lateral (x−, y) and up to...
500 nm axial (2) resolution due to the spatial filtering technique. This technique allows optical slicing of the sample and construction of a three-dimensional image without collection of out of focus light. This feature allows to image for example cells, tissues, 3D scaffolds/spoanges, which showed promise in copious application, including microfluidics and flexible electronics, or nanostructures and subsequently illustrate them 3-dimensional. Nowadays, the research is shifting towards nanotechnology (for example nanocontainers) and fundamental biology of cells, which are in a size-range of tens to few hundred nm. Here, optical microscopy methods lack sufficient resolution due to the diffraction limit described by Abbe. Several attempts to overcome the diffraction limit were successful. These methods are introduced briefly in the following paragraph.

2.1 Super-resolution techniques

The general name of approaches overcoming the resolution limit is super-resolution fluorescence microscopy. As an emerging method, the super-resolution reversible saturable optical linear (fluorescence) transitions (RESOLFT) microscope has to be mentioned, as it is suitable for in vivo studies. STED (stimulated emission depletion) and ground state depletion (GSD) microscopy rely on the working principle of RESOLFT. As STED is a well-established method, since Stefan Hell received the Nobel Prize in Chemistry in 2014 for his outstanding work in super-resolved microscopy, this technique is shortly introduced here. However, other – not less intriguing – super-resolution techniques include PALM (Photoactivated Location Microscopy), FIONA (Fluorescence Imaging with One Nanometer Accuracy), a method for accurately determining the position of a fluorophore by ascertaining the center of its emission pattern, and STORM (Stochastic Optical Reconstruction Microscopy), a stochastic approach based on FIONA and relying on the transfer of the majority of fluorophores to a non-fluorescent dark state. In STED, two well-aligned lasers are used. The first laser possesses the typical Gaussian beam profile and is used to excite the fluorophores in the sample, whereas the second laser possesses a donut-shaped beam profile and is used to de-excite all but the fluorophores in the center of the beam. Afterwards, the fluorescence emission of molecules in this small region (smaller than diffraction limit) is detected. As STED is a scanning technique, the image is generated by moving the beams over the sample while recording the fluorescence intensity. A lateral resolution of down to 2.4 nm was reported recently. Typically, the resolution is in the order of tens of nanometers. The resolution can be adjusted by the intensity of the depletion pulse, the lateral STED-enhanced resolution/PSF (point spread function) is given by eqn (1). The axial resolution, however, remains for a typical experiment rather low (approx. 40–500 nm).

\[ d_{\text{STED}} = \frac{\lambda}{2NA \sqrt{1 + 1/I_{\text{Sat}}}} \]  

Here, \( \lambda \) is the wavelength of the excitation light, \( NA \) is the numerical aperture of the objective, \( I \) is the intensity of depletion light, and \( I_{\text{Sat}} \) is a fluorophore-dependent parameter defined by the intensity of light required to suppress 50% of fluorescence. During STED measurements it is feasible to determine the excited state lifetime of a fluorophore or even multiple fluorophores, but the initial part of the fluorescence decay is difficult to analyze as it is compromised by the action of the STED beam, rendering the decay multi-exponential. It contains fluorescence photons from fluorophores located further away from the doughnut zero and is therefore not super-resolution. Hence, the first two nanoseconds of the time-correlated single photon counting (TCSPC) decay are typically discarded under the premise that organic dye molecules have a fluorescence lifetime in the order of 2 to 5 ns. The feasibility of STED/FLIM was shown by B"ucker et al. They used a two-channel STED imaging system and fluorescence lifetime separation was applied. Tubulin and lamin were immunostained with ATTO 647N and KK 114, respectively. By fitting each pixel with a biexponential decay of fixed lifetimes (1.8 ns and 3.1 ns) the structures of tubulin and lamin were well separated.

The drawbacks of STED are, that (a) only a small variety of fluorophores may be used for STED due to their stability against photo-bleaching and (b) short fluorescence lifetimes i.e. of samples with a high concentration of reporter dye (self-quenching) cannot be determined with a high accuracy due to the STED-induced decay. Also the analysis of the amplitudes will yield in falsified results as the decay is not used between 0 and 2 ns after the excitation pulse. Here, the normal fluorescence lifetime imaging microscopy has an advantage over the STED/FLIM as the instrument response function (IRF) is well defined and for fitting the excited state lifetimes the whole decay may be used, which yields in high accuracy of short lifetimes and a quantitative analysis of different populations. Therefore, other techniques and combinations of measurement techniques are developed or are used.

2.2 Coupling far-field optical microscopy and its variations with the AFM

2.2.1 How to combine optical microscopy and AFM? The sample preparation for fluorescence microscopy and confocal laser scanning microscopy is facile and fast. However, often staining or usage of reporter dyes is needed (see for example the inspiring topical review by Dean and Palmer). Samples can be measured in solution, which makes it a versatile method for analyzing biological samples at physiological conditions. Therefore, CLSM and fluorescence microscopy are frequently utilized in biology (e.g. cellular structure, localization of ions/macromolecules and tracing specific cell) and medicine (e.g. dentistry, stem cells, human cornea and in vivo confocal microscopy). The applications are not confined to biological samples, rather CLSM is utilized in a broad range of applications, including polymer chemistry (diffusion coefficient) and surface chemistry (adsorption of (macro)molecules).

Fig. 2 shows different acquisition modes. The two major methods of data acquisition of a combined measurement are either concomitant (Fig. 2a) or successive (Fig. 2b). Some
Fig. 2 Modes of operation of the atomic force fluorescence microscope (AFFM): (a) simultaneous imaging by scanning the sample between a fixed tip and a fixed focus; (b) AFM imaging by lateral tip scanning with a specific ROI in the excitation volume; (c) force-extension imaging with the tip moving in three dimensions; (d) force-extension imaging with the tip ramping perpendicular to the surface and the sample moving in lateral directions. Reprinted with permission from ref. 44 Copyright (2005) John Wiley and Sons. (e–f) Beam diagnostic camera images of back-reflected light from the sample surface with the AFM tip retracted (e), with AFM tip visible as a distortion (f) and after alignment (g). For all images, the focus had been moved towards the AFM tip to show the distortion of the pattern more clearly. Reprinted with permission from the authors and ref. 110 Copyright (2010) Society of Photo-Optical Instrumentation Engineers.

measurements or analysis are even made comparative, meaning AFM and optical measurements may not be at the same position of the sample (not aligned). A researcher should decide carefully if it is favorable to measure simultaneously or execute the measurements successively. A combined measurement may save time and an interaction of the tip with the sample may be observed due to tip-enhanced fluorescence or tip-induced quenching.\(^{57,108}\) This may be desired to determine the location of a dye molecule on a surface or in a polymer matrix. On the other hand, the determination of fluorescence properties of fluorophores and the topography measurement have to be conducted successively to extirpate undesired changes in the fluorescence properties of the fluorophore.

To combine far-field optical microscopy techniques, such as fluorescence microscopy, confocal microscopy and FLIM or other methods, such as total internal reflection fluorescence (TIRF), fluorescence correlation spectroscopy (FCS) and super-resolution techniques, with the AFM a specific setup is needed, which has to be aligned perfectly (up to a few nanometers). The combined AFM-optical microscopy technique consists out of a sample scanning AFM and an inverted microscope (e.g. CLSM). The microscope can be equipped with different excitation wavelengths. For optical detection with high resolution, an (oil) immersion objective with a high numeric aperture (1.45 or even higher) can be utilized. The link between the two measurement systems is the AFM sample stage, which is mounted directly on the inverted microscope chassis replacing the original sample stage. The sample stage has to be mounted carefully onto the inverted microscope, especially, taking into account the necessary space needed for the objective of the microscope, as well as its operating distance. It might be necessary to insert spacers. This setup allows measuring concomitant or successively optical microscopy and AFM.

For alignment of the orthogonal methods, first, the cantilever tip is adjusted to the cross hairs in the eyepiece of the microscope by manual positioning of the sample stage. Now, the cantilever tip is brought into contact with the surface and the microscope is adjusted to measure backscattering light. Keep in mind to reduce the excitation intensity to protect the detector. Acquired images of the backscattering of the cantilever indicate the position of the tip. The tip apex is typically visible in the backscattering images as a bright spot.\(^{59}\) Alternatively, the scattering of the incident light, which can be observed by a CCD camera (beam diagnostic camera, see Fig. 2e–g), can be utilized for fine adjustment, if the tip apex is not visible in the backscattering image.\(^{109}\) The quality of alignment is in this process clearly visible in the distortion of the reflected light originating from the retracted tip (Fig. 2f). Rather a strong distortion of the symmetry is observed for a misaligned setup, while high symmetry of the backscattered light is obtained for a well-aligned (AFM tip in the center of distortion pattern) setup, as shown in Fig. 2g.

2.2.2 AFM-combined with fluorescence microscopy and confocal microscopy. Numerous attempts to combine the AFM with optical fluorescence microscopy have been made. An early combination of confocal microscopy with an AFM was constructed in 1994 by Neagu et al.\(^{111}\) They were able to measure human lymphocytes, which were sequentially labeled with FITC and immunogold, with a combination of AFM and optical fluorescence microscopy. The images showed good correlation and they were able to determine optimal imaging conditions for both the AFM and the microscopy by varying the thickness of immunogold and silver enhancement.\(^{111}\) Another combination of optical microscopy with AFM was developed by Lieberman et al.\(^{112}\) They integrated near-field optical microscopy and far-field microscopy into an AFM. The instrument had the capability to measure normal force and shear force, as well as subdiffraction limit fluorescence intensity (NSOM) and it was capable to optically slice the desired ROI (confocal microscope).\(^{112}\) Consequently, after these first attempts to combine the two methods, such hybrid instruments were utilized in biological imaging of cells, filaments, proteins, cytoskeleton and nucleotides, and in biophysics, for example for the analysis of structural and dynamic changes in lipid bilayers.\(^{113–121}\)

A problem for combined AFM and microscopy measurements in the past was the presence of background noise in microscopy images, which is related to the laser utilized for the AFM optical lever.\(^{122}\) This is bypassed either by measuring consecutively or by measuring concomitant while using a high-quality filter.\(^{122}\) While utilizing filters, a potentially useful part of the spectrum cannot be analyzed due to the blocking of these wavelengths. This is especially a problem for microscopic
systems, utilizing the emitted fluorescence light for generation of spectra. By employing a laser with a wavelength of approx. 1050 nm for the AFM, the background in microscopy images as well as problems with photobleaching or un_specific excitation of the sample can be avoided.\textsuperscript{121} Kassies et al. designed such a combination of an AFM with a confocal microscope (atomic force fluorescence microscope (AFFM)), where the AFM laser was shifted to a wavelength of 1050 nm. They constructed an AFFM with the capability of measuring simultaneously topography and fluorescence images, and the capability to measure fluorescence spectra at specific points of interest. They showed that they can measure on membrane fragments from \textit{Rhodobacter sphaeroides}, containing both LH1 and LH2 (LH = light-harvesting pigment–protein complex).\textsuperscript{123} Furthermore, they demonstrated that measurements in a combined optical and force extension/nanomanipulation mode is possible with their setup.\textsuperscript{125}

As shown previously, the exact alignment may be difficult and time-consuming. Another problem during a combined experiment is the drift in an AFM during measurement,\textsuperscript{121} which necessitates keeping an eye on the alignment of the measurement equipment. Timmel et al. utilized an alignment correction method, which uses the cantilever tip as a reference landmark.\textsuperscript{124} At first, they validated their method with beads in a complex artificial sample and subsequently, the method was utilized to maintain alignment during measurement of membrane structures in fixed and living human fibroblasts (biological sample). They showed that the fluorescence signals and the topographic structures were well-aligned and that nanoscale membrane structures could be related to the fluorescence spot.\textsuperscript{125}

Lately, Staunton et al. presented a method for quantitative mechanical characterization of soft, heterogeneous samples in 3D via a combination of AFM, CLSM and finite element analysis (FEA). They showed the capability of their combined technique for the quantification of the elastic properties of cells (here metastatic breast adenocarcinoma) in an extracellular matrix (here collagen hydrogels). With this method, it is possible to decouple the response of a cell from its soft surrounding (extracellular matrix, ECM). By this means, although the response of the indentation experiment is based on both, the cell and the soft surrounding, the elastic properties of the cell and the ECM can be determined quantitatively.\textsuperscript{126}

2.2.3 A combination of AFM with fluorescence lifetime imaging microscopy (FLIM). Fluorescence light possesses both frequency and time-domain. A combination of the AFM with a confocal fluorescence microscope working in the time domain (i.e. time-correlated single photon counting) enables the direct measurement of topography, fluorescence intensity and fluorescence lifetime. Since 1926 it has been possible to determine the excited state lifetime of fluorescence ($\tau$), another basic fluorescence parameter.\textsuperscript{127}

The fluorescence lifetime (decay time, eqn (7)), $\tau_F$, can be defined by use of a simple kinetic scheme (first-order rate constants), where all radiative (fluorescence, eqn (3)) and all nonradiative pathways (inter system crossing (ISC), internal conversion (IC), dissociation) have to be considered.

\[
\begin{align*}
M + h\nu & \rightarrow ^1M^* \times I_a \quad \text{(absorption)} \\
^1M^* & \rightarrow M + h\nu \times k_R \quad \text{(fluorescence)} \\
^1M^* & \rightarrow ^3M^* \times k_{ISC} \quad \text{(intersystem crossing)} \\
^1M^* & \rightarrow M \times k_{IC} \quad \text{(internal conversion)} \\
^1M^* & \rightarrow \text{products} \times k_D \quad \text{(dissociation, bleaching)}
\end{align*}
\]

Here, $k_i$ depicts the rate constants of the processes shown in eqn (3)-(6). From the steady-state analysis of the eqn (3)-(6) the fluorescence decay time $\tau_F$ is given by eqn (7).

\[
\tau_F = (k_R + k_{IC} + k_{ISC} + k_D)^{-1}
\]

There are several techniques to determine the decay times of fluorescence. The most common technique is TCSPC. It relies on the accurate time measurement of single photon events (e.g. fluorescence). The laser pulse serves as a reference for the start time, whereas the stop time is determined by the fluorescence photon. These photon detection events are binned and converted into a histogram. For this histogram, a small time bin down to 1 ps is used. The photon events are collected by adding +1 in the time bin proportional to the start-stop time. After many cycles, the distribution of such detection times builds up.\textsuperscript{126-128} Afterwards, the data can be analyzed by eqn (8) (exponential decay).

\[
A(t) = \sum_i \alpha_i e^{-t/\tau_i}
\]

The fluorescence lifetime values can yield information about the molecular environment of a fluorescent molecule, \textit{i.e.} viscosity,\textsuperscript{129,130} pH,\textsuperscript{131} temperature,\textsuperscript{132} polarity\textsuperscript{133,134} and solvation.\textsuperscript{135} Furthermore, the excited state lifetime of a fluorophore can be altered by ionic strength,\textsuperscript{136} oxygen concentration,\textsuperscript{137} binding to macromolecules, changes in protein orientation, change in protein folding,\textsuperscript{138} a critical binding reaction\textsuperscript{139} and the proximity of molecules that can deplete the excited state by resonance energy transfer (RET).\textsuperscript{138,139} Therefore, fluorescence lifetimes can be utilized as indicators of these parameters. There are various applications utilizing fluorescence lifetime, \textit{i.e.} in calcium and other chemical detection,\textsuperscript{140} clinical detection\textsuperscript{142} and determination of transport processes (diffusion).\textsuperscript{141,142} Although FLIM is typically featured in biological studies, it also finds application in polymer science and surface analysis.\textsuperscript{109,145} A combination of FLIM with AFM potentially yields information of biological processes occurring inside cells, which would not be possible without FLIM.

Recently, a few articles concerning themselves with this kind of combination, which belong to an a-SNOM approach, were published. An advantage, which was exploited in these articles, was the higher optical resolution due to short ranged tip-induced quenching and inherent fluorescence lifetime decline. Schulz et al. dried a diluted sample of ATTO 647N on a clean glass slide. The density of the dye molecules was in the order of 1 molecule per $\mu m^2$. During the measurement in the
combined mode, the diffraction limited spots of the fluorophores show typical single molecule features like blinking and beaching. All fluorescence spots possessed a dark area in their center, which were typically in the order of 20–40 nm FWHM. The dark areas were attributed to energy transfer to the AFM tip. Here, the excited state lifetime changed by advancing the tip towards the organic dye. A drop of excited state lifetime with decreasing distance was observed. Thus, this setup possesses the ability to measure with high resolution without the need of tedious and sophisticated super-resolution equipment, such as specialized dyes, optics, and lasers. A few years later, single digit nanometer resolution via the same approach was shown (see Fig. 3). Concomitantly, the fluorescence lifetime information yielded knowledge about the orientation of the dye molecules. Schulz et al. found that the molecular transition dipole moments lie parallel to the sample surface. AFM (intermittent mode) and FLIM were also used by Yoskovitz et al. CdSe quantum dots coated with multiple shells (7.3 nm diameter) were placed onto a cleaned glass surface. AFM was measured in tapping mode isochronal with fluorescence intensity and the time-correlated single photon counting data. The obtained data showed a fluorescence enhancement for silicon tips at approximately 100 nm laterally away from the fluorophore. This data is in agreement with the literature, where the fluorescence enhancement is assigned to a field enhancement at the apex of the tip. Furthermore they showed that excited state lifetime yields in an enhancement of the signal-to-noise ratio, and also significantly improved resolution.

Lately, a combination of AFM-FLIM in a far field approach was utilized to study surface nanobubbles. Surface nanobubbles are nanocavities filled with gas (air), which nucleate at the interface between solids and liquids (typically water). For this approach water was stained with Rhodamine 6G (Rh6G). Rh6G appeared to be enriched at the liquid–gas interface, which developed during nanobubbles nucleation, as shown in Fig. 4b. The surface nanobubbles appeared brighter in the confocal fluorescence microscopy images than the interphase (glass–water) without nanobubbles (compare Fig. 4d and g). The fluorescence intensity image (bright nanobubbles) and the topography image of the nanobubbles were in good agreement. Here, the excited state lifetime analysis served as proof of a water–air interface. TCSPC decays measured at the location of

Fig. 3  (a) Scheme of hybrid AFM-FLIM setup. (b) Scheme of tip-induced quenching and course of intensity versus separation distance between tip and fluorophore. (c) Fluorescence intensity data of a sample containing single dye molecules (ATTO 655) with the AFM tip approached to the surface. (d) Magnification of (c). (e) Same ROI as in (d) is imaged with retracted tip. The scale bar for (c) is 2 μm and for (d) and (e) 500 nm. For (f), (g), (h) the FWHMs are 6.8 nm, 7.5 nm, and 5.9 nm, respectively. (i) Triangle shape due to a blunt tip. (j) Fluorescence lifetime distribution, the calculated fluorescence intensity and the measured fluorescence intensity of a quenching spot with a FWHM of 16 nm is shown. (k) Scheme of the physical mechanism leading to quenching. Reprinted from open-access article ref. 58 under the terms of the Creative Commons Attribution License.
a nanobubble yielded a tri-exponential decay, whereas TCSPC decays on the substrate–solid interface (without nanobubbles) yielded a bi-exponential decay (compare Fig. 4e and h). The third excited state lifetime, which was approx. 0.6 ns, was attributed to the liquid–air interface, as this lifetime is not present in a sample without nanobubbles.\textsuperscript{109} Prior to this, the existence of this air/water interface was discussed in the academic community as these nanobubbles would be unstable due to high inner pressure (curvature).\textsuperscript{148}

He et al. employed AFM correlated with single-molecule fluorescence intensity/lifetime imaging microscopy (their acronym: AFM-SMFLIM) to investigate interfacial electron-transfer processes of a mixed \((m\text{-ZnTCPP}/\text{TiO}_2\text{ nanoparticles}) + m\text{-ZnTCPP})/cover glass sample. The correlated information of fluorescence blinking of each individual dye molecule and its fluorescence lifetime along with the surrounding topography explained the coupling strength inhomogeneity of each dye molecule with \text{TiO}_2 nanoparticles (NPs) and its effect on

---

**Fig. 4** (a) Scheme of the hybrid AFM–FLIM microscope. (b) Scheme of the partitioning of the fluorophore Rh6G at the interface and in water. Nanobubbles nucleated by an ethanol–water exchange on the piranha-cleaned glass in an aqueous 850 nMRh6G solution: (c) AFM height image; (d) confocal fluorescence microscopy intensity image in the same ROI as in (c). (e) TCSPC fluorescence decay curve of Rh6G obtained from TTDTR data of panel (d). (f) AFM height image and (g) confocal fluorescence microscopy intensity images of UV-ozone cleaned glass after the ethanol–water exchange in aqueous Rh6G solution (850 nM). (h) TCSPC decay curve of Rh6G obtained from TTDTR data in panel (g). Reprinted with permission from.\textsuperscript{109} Copyright (2016) American Chemical Society.
electron transfer intermittency and thus, yielded molecular level understanding of the interfacial electron transfer reactivity.159

2.2.4 AFM coupled to fluorescence correlation spectroscopy (FCS). Only a few studies were published for combinations of AFM with FCS,150–154 although combinations of AFM and confocal fluorescence microscopy are utilized in the past 20 years (see above). This may be related to the application of FCS, which is utilized to measure quantitatively dynamic parameters, such as chemical reaction rates,155 diffusion coefficients,156 hydrodynamic radii,157 (average) concentration158 and single-triplet transitions.159 Furthermore, reasons for its scarcity are a mismatch of acquisition times and difficulties with the alignment on the soft interface, which exacerbates the issue of drift in AFM during a combined measurement. These problems may be the reason for predominantly comparative measurements of AFM and FCS.160 Evidently, FCS is orthogonal to the AFM technique.

A combination of these two techniques was utilized typically in the analysis of liquid films and membranes.150,151 The first study utilizing AFM-FCS was done by Burns et al. in 2005. It was utilized to analyze the relative partitioning and the mobility of labeled probes in gel and disordered liquid phase of bilayers consisting of 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC) lipid domains in 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC).152 For their analysis, at first, sites with different domains were mapped by combined AFM and CLSM measurement, allowing the correlation of topography (AFM) with probe partitioning between gel and liquid domains (CLSM). The FCS analysis showed that two components are present in the DOPC fluid phase (fast and slow), which was ascribed to membrane heterogeneities.150 Subsequently, in the group of Schwille, the AFM-FCS technique was utilized to characterize dynamic and structural organization of phase-separated membranes153 and to show coexistence of the liquid disordered and liquid ordered phase for ceramides, which forms gel-like domains.154 The formation of these ceramide-rich domains was found to be dependent on the acyl chain length of the ceramide.153

2.2.5 AFM coupled with total internal reflection fluorescence (TIRF) microscopy. Total internal reflection fluorescence microscopy makes use of the total reflection of light, which happens at an excitation incidence angle greater than the critical angle, and the thereby originating evanescent field. Fluorophores near to the total reflection (glass surface) are selectively excited by interaction with the evanescent field.162 Fluorescence from these excited molecules can be collected by the microscope optics. The advantage of TIRF over a conventional CLSM/optical microscope and even super-resolution techniques (STED) is the high axial resolution of up to 100 nm (compared to approx. 500 nm in CLSM), which can be enhanced by multigate or multiwavelength techniques up to approximately 20 nm.163,164 Therefore, TIRF has applications for minute structures or molecules, which are located near to a surface (glass slide), as this technique enhances the signal to noise ratio. Such applications are for example surface nanobubbles,164 cell imaging165 and dynamics of membranes.166 Similar to a combination of CLSM and AFM, a combination of TIRF with AFM provides complementary benefits for sample characterization. The enhanced signal to noise ratio and the high sensitivity makes the TIRF-AFM combination especially useful for accessing high-resolution structural information of proteins or filaments,167 arrangement and orientation of these molecules,168 nanomanipulation169 and modulation (enhancement/quenching) of fluorescence similar to experiments with the CLSM.170

Many publications rely on the superior lateral and axial resolution of AFM over TIRF and the single photon accuracy of TIRF.166,171 These qualities were employed in the study of myosin labeled with tetramethylrhodamine-5-maleimide.168 Myosin self-assembled to asymmetric filaments. The cross-correlation of AFM and TIRF (height/volume vs. intensity) yielded structural information of the assembly. The intensity versus height ratio implies that myosin heads form a shell around the filament axis, which is consistent with the heads exposed to the outside.168 Although TIRF is the technique with lower resolution, it was capable to detect the association of β-amyloidDOPC/DPPC lipid bilayers earlier than AFM.171

AFM is often exploited for its force measurement capability and its ability to manipulate microscopic objects (micromanipulation) or even manipulation on an atomic scale (nanomanipulation).169,172–174 Such an application is the single cell manipulation via AFM to study the integrin Mac-1(cell)-fibrinogen interactions in comparison to the intermolecular fibrinogen interactions.172 Force transmission, number, and arrangement of focal adhesion points of the cells can be analyzed by exerting a force on the apical membrane of cells, which adhere to a transparent and thin surface.173 Recently, TIRF was utilized to stimulate a single T cell by light (via photoactivatable Rac protein) while simultaneously the mechanical response of the cell was measured via AFM.175 This method depicts an inverted approach of the AFM-TIRF setup, as typically the AFM is utilized as a nanomanipulator. Single cells could be seeded with fluorescent beads (fluorescent nanoparticles), which could be imaged subsequently with the TIRF setup.175 An interesting approach to monitoring the genome release of adenovirus capsids was shown by Ortega-Esteban et al. In their research, similar to CLSM and FLIM essays for release studies, the rupture and release of fluorophores was observed by TIRF while the virus membrane was weakened and finally ruptured by the AFM (active trigger, see Fig. 5).174 They could show that the loss of the initial penton in frame 7 leads to a marginal incline in fluorescence but not to a reduction in height, whereas the rapid decrease of height after frame 17 signals the start of the complete disassembly, accompanied by a strong increase in fluorescence intensity.174 By advancing towards fluorescent nanoparticles/molecules, fluorescence modulation techniques similar to CLSM can be utilized. Eckel et al. used fluorescent CdSe nanocrystals and gold-modified AFM tips to enhance the emission, the tip-nanocrystal distance for maximum emission was 22 nm, or to quench emission effectively.170 Here, the enhancement was attributed to resonant exciton-plasmon coupling.176 An enhancement of the previously mentioned method could be achieved by Lee et al. as they compensate for the photo brightening effect, which enables quantitative measurements.177
2.3 AFM coupled to super-resolution techniques

A further improvement of the AFM-CLSM combination was achieved by adopting super-resolution techniques, such as STED, FIONA, dSTORM and PALM. Such a combination has several advantages, amongst others, other fluorescence-based techniques can be adapted at least for the STED, such as FCS, FLIM, fluorescence recovery after photobleaching (FRAP), multicolor imaging and steady-state fluorescence probing. Via super-resolution techniques the lateral and axial resolution is enhanced up to 20 nm and 100 nm, respectively, rendering subcellular structures observable in detail. Higher optical resolution was observed for non-commercial setups. Similar to an AFM-CLSM combination, the AFM-super resolution techniques benefit from the fast acquisition times of the optical method, although nowadays special AFM equipment is available with high temporal resolution. Therefore, this combination tracking of several small molecules in close proximity, is possible (super-resolution technique) and simultaneous either nanomanipulation, determination of change in morphology or viscoelastic properties of a sample. Similar to the CLSM, the chemical information/ surrounding of a fluorophore can be evaluated, which proves to be difficult via the AFM. However, biomolecules and polymers are invisible to single-molecule localization microscopy (SMLM) as it only detects fluorophores with a specific absorption range and has to be stained. Furthermore, the z-resolution in SMLM methods is still in the order of 100–500 nm, although advances in SMLM for example via a mirror-reflected approach yield in higher axial resolution. The successful combination of STED with AFM was first reported in 2012 by Harke et al. As the used experimental setup is similar to the setup for a combined AFM-CLSM experiment the representation of the setup was waived. AFM-STED was demonstrated at first for 40 nm fluorescing crimson spheres at dry and wet conditions. Subsequently, microtubules of Cos7 cells labelled with Atto 647 N were imaged and correlated to mechanical variations in the Young’s modulus (see also Fig. 6). Chacko et al. showed that measurement artifacts of the optical image can be accounted for by AFM and the images can be corrected afterwards, i.e. by calibration via a Labview procedure. Furthermore, AFM subdiffraction nanomanipulation of fluorescent crimson microspheres visualizes the high-resolution targeting capability of the system. Jianqiang et al. facilitated the combined setup by utilizing a super continuum laser and for the first time concomitant and synchronized optical and topographic images were obtained. They applied their setup for nanobeads with a resolution of 42 nm as well as cells. Recently, dSTORM and PALM were combined with the AFM to measure Factin (dSTORM) and living mammalian cells (PALM). While the AFM images illustrate the dynamics of the cell membrane a PALM series monitors the changes in protein clusters over time. Similarly,
2.4 Near-field optical microscopy (SNOM/NSOM)

The idea of SNOM was probably first conceived by Ash et al. in 1972. By use of 3 cm microwave radiation, a resolution of \(\lambda/60\) in one dimension and \(\lambda/20\) for two-dimensional objects was achieved, but technical difficulties prevented the extension of this technique towards shorter wavelengths. 2007 by Oshikane et al. the lateral and vertical resolution was determined to be 20 and 5–2 nm, respectively. SNOM is a nano-optical imaging technique that enables light–matter interaction for the purpose of extracting relevant information about nanoscale objects. There are two inherently different methods in scanning near-field optical microscopy. One can make use of a sub-wavelength aperture from which excitation light emanates or through which the emission from the sample is detected, or both. This is called aperture SNOM. The resolution in aperture SNOM is proportional to the radius of the aperture. However, as the aperture size decreases the amount of light admitted into the aperture decreases as well and signal levels drop. This results in a trade-off between signal levels and spatial resolution leading to a practical resolution limit for aperture SNOM of \(\lambda/10\). The other method is executed by probing highly localized interactions of excitation and emission photons with a sub-wavelength structure. These structures are usually in the range of a few nanometers to a few tens of nanometers (aNSOM or NSOM). However, the contrast mechanism is not fully understood and images may contain topographical artifacts. Apertureless NSOM is typically measured via a bottom-illumination mode, which yields in advantages in light confinement and background noise reduction. As the probing tip has to be in close proximity to the glass surface, the measurement by aNSOM is restricted to thin samples, which diminishes its applicability. Recently, an aNSOM was developed with the capability to measure via bottom-illumination and top-illumination mode, as well as a measure in water and in air. The resolution was found to be independent on the illumination mode, but was lower in water (32 ± 7 nm) than in air (25 ± 6 nm). Furthermore, the resolution can be enhanced by amplifying the incident and scattered electric fields at the tip itself. These results indicate that aNSOM in top-illumination mode (also called s-SNOM) is able to measure thicker samples, which are not measurable via the bottom-illumination mode. Both, the setup of apertureless and aperture NSOM are shown in Fig. 7, indicating the different approaches to enhanced resolution.

Nowadays, s-SNOM is coupled to IR to resolve intermolecular interactions with nanometer spatial resolution, which is yet, similar to PTR, another method to chemically identify surfaces with high spatial resolution. This field is under vast development and recently numerous research articles were published. For example, Pollard et al. investigated as a proof of principle the self-organization of amphiphilic block copolymers into hydrophilic and hydrophobic domains. By their approach, they were able to chemically map the surface with high spatial resolution while obtaining exquisite sensitivity, which can be used for the unravelling of intra- and intermolecular interaction (see Fig. 8). Still, SNOM methods are burdened with various artifacts, i.e. due to a broken or blunt tip. There is up to now no method to evaluate if an image is without an imaging artifact. As SNOM relies on the concomitant measurement of the optical and force microscopy, a fast and simple survey scan similar to typical optical microscopy is not possible anymore. On these grounds and because aperture SNOM is still often utilized (more artifacts, lower resolution compared to other methods) a combination of conventional optical microscopy may be favorable to SNOM and s-SNOM, especially for large three-dimensional samples (optical slicing ability). Applications of NSOM/NSOM and the novel s-SNOM are mostly biological appliances, such as cell visualization and analysis. However, also applications in microscopy for materials are well known for example, analysis of semiconducting heterostructures, such as quantum dots, quantum wires and disordered quantum wells, material imaging, e.g. local crystal structures, crystal defects and doping and observation of intra- and intermolecular interaction in both biological and material science fields.

2.5 AFM & Raman spectroscopy – tip-enhanced Raman spectroscopy (TERS)

Raman spectroscopy is the complementary technique to IR spectroscopy as most vibrations are either Raman or IR active,
and it is also orthogonal to AFM as Raman is able to gather chemical information of a desired sample.\textsuperscript{216,217} The former refers to the different selection rule compared to IR. Raman occurs mainly for symmetric vibrations when the polarizability changes upon excitation. Raman spectroscopy relies on the inelastic scattering of monochromatic light (nowadays laser),
while the molecule (sample) is excited to a virtual energy state. From this state, an inelastically scattered photon emanates, which can possess either higher (anti-Stokes) or lower (Stokes) energy than the incoming photon. The difference in energy of the resulting scattered photon can be related to the energy differences in the rotational and vibrational states. Raman spectroscopy is widely utilized in chemistry and material science, as chemical bonds, functional groups and even different hybridization states are detectable. Especially, it is utilized in applications related to analytical chemistry, forensic science (analysis of drugs or paints), geology and mineralogy (e.g. gemstone identification), biology (e.g. secondary structure of polypeptides/proteins, phospholipids), material science (e.g. semiconductors, carbon materials and polymers) and life science (e.g. pharmaceutical analysis).

Tip-enhanced Raman spectroscopy (TERS) combines the chemical sensitivity of surface-enhanced Raman spectroscopy (SERS) with the high spatial resolution of the AFM to concomitant garner chemical and morphological information at the nanometer length-scale. TERS is a near-field microscopy technique in which the Raman signal is enhanced by an apertureless probe. The probe is a sharp metal-coated AFM-tip, which is positioned at the center of a laser focus. The enhancement of the electromagnetic (EM) field and therefore of the Raman signal can be ascribed to a combination of localized surface plasmon (LSP) resonance and lightning rod effect. The enhancement effect is confined to the vicinity of the tip-apex. Hence, TERS overcomes the resolution limit conventional Raman spectroscopy is bound to. The resolution of TERS is typically in the order of 20 nm (see Fig. 9), but can be enhanced by specific reflection modes up to 1 nm.

TERS has been utilized in a broad range of applications in biology, such as pathogens, cell membranes and peptides, in materials science, such as polymer blends, and chemical engineering, i.e. in catalysis for detection of intermediates or as a trigger for chemical reactions. For example, Kumar et al. investigated in situ photocatalytic oxidation of (p-mercaptoaniline) pMA (p-p’-dimercaptoazobenzene) DMAB on gold nanoparticles with TERS (see Fig. 10c-f). Compared to far-field Raman spectroscopy, the integration time could be reduced while the peaks are more pronounced due to the enhancement effect in TERS, as shown in Fig. 10d and f. Due to the broad spectrum of TERS and its applications a thorough illustration of TERS would fill another review by its own. Therefore, we want to refer the interested reader to the reviews of Kumar et al. and Jiang et al., which summarize recent advances in TERS together with its advantages and weaknesses. TERS itself is developed further, even though it is already utilized for many applications. Important issues, which are encountered, are low fabrication reproducibility of the AFM-tip, which becomes manifest in differing Raman enhancement factor or induced plasmonic dipole factors from tip to tip, short plasmonic lifetimes, which are assigned to metal delamination (Au-tips) or chemical alteration (Ag-tips) and low signal-to-noise ratio due to far-field scattering/emission. Extensive research was performed on solving these issues.

Improved fabrication reproducibility of the tip was achieved by utilizing an increased amount of wet-chemically synthesized silver nanowires (AgNWs), which are bound to the apex of the tip. This leads to improved electric contact, mechanical strength, and reproducibility, which can be exploited by the commercialization of such modified tips. However, TERS probes relying on Ag-tips were found to lose the plasmonic enhancement of the tip during the first 4 hours of exposure to the environment (oxygen/humidity). It was shown that the lifetime of a TERS-tip based on Ag can be maintained up to 5 months by utilizing an environment with sub-ppm oxygen and moisture concentration (typically in a glovebox). It was also mentioned that Ag based tips can be protected for storage and measurement either by the inert atmosphere with previous mentioned low oxygen content and low humidity or by covering the tip with a thin (≤3 nm) layer of alumina. Furthermore, enhancement of TERS can be achieved by change of the illumination geometry, resulting in an even improved TERS signal, which was observed for Raman spectra of malachite green iso-thiocyanate and thiophenol in water and in air (see Fig. 10a-f), and tip modification, which renders the combined setup sensitive to pH change.

### 2.6 AFM & IR-spectroscopy – photothermal-induced resonance (FTIR) and infrared photoinduced force microscopy (IR-PiF)

IR spectroscopy is one of the oldest and widespread analysis techniques for the analysis of solid samples. However, IR spectroscopy can be also utilized for liquids, soft matter and gases to identify chemical species. It is based on the absorption of light from the spectrum of a light source. Nowadays, IR is measured via the Fourier-transform technique also known as Fourier-transform infrared spectroscopy (FTIR), which enables fast and highly accurate measurement of whole spectra. Molecule vibrations, which change the dipole moment of the molecule, are IR active and may absorb light of a specific wavelength. This absorption of a specific wavelength can successively be translated into specific bonds of a molecule or related to small molecules themselves. Recently, the FTIR technique was enhanced by coupling it to an optical microscope. This results in FTIR microscopy with a lateral resolution of down to 10 µm (compare diffraction limit). In an actual experiment, this value is with a scan size of 20 × 20 µm bigger, as it is difficult to obtain a good signal to noise ratio and enough IR radiation. The most important operation modes of FTIR are transmission, diffuse reflectance infrared Fourier transform (DRIFT) and attenuated total reflectance (ATR). The transmission mode can be utilized for gases, liquids, and solids, whereas the ATR method can only be utilized for liquids and solids. For a thorough explanation of FTIR and IR, its mathematics and its operation modes please refer to standard textbooks, e.g. "Fourier Transform Infrared (FTIR) Spectroscopy."

IR and FTIR spectroscopy are widely utilized in biology/biophysics (e.g. protein conformational changes), environmental science (e.g. gas analysis), chemistry (e.g.
identification of molecules or polymers and chemical reactions in the gas phase, surface analysis (e.g. surface contamination, thin film analysis and analysis of surface termination) and polymer analysis (e.g. degree of crystallinity).

A combination of AFM with infrared spectroscopy or typically Fourier transform infrared spectroscopy is called AFM-IR, but often it is abbreviated PTIR (photothermal-induced resonance) due to its working principle. Dazzi et al. developed the concept of PTIR in 2010. PTIR relies on the excitation of molecules (vibration) by a tunable pulsed IR laser. The infrared light emitted from the pulsed IR laser is absorbed by the molecules leading to a quick thermal expansion. This expansion induces an oscillation of the AFM cantilever, which is detected via the deflection of the detection laser beam. By utilizing a Fourier transformation, frequencies and amplitudes can be acquired. Here, the obtained amplitudes are related to the strength of the cantilever oscillation. Studies utilizing PTIR have analyzed the chemical information of biological samples, such as proteins, lipids and lipid vesicles, cells, bacteria, polymer samples and thin films, medical devices, drugs, nanostructures, metal-organic frameworks (MOFs), organo-halide perovskites, and nano-patterned metals at a resolution up to 50 nm. Here the improved resolution of the PTIR serves to analyze nanoscale regions of relatively thin samples. The amplitude of the PTIR signal ($S$, see eqn (9)) is dependent on the sample thickness ($z$), absorbed energy per unit area ($U_{abs}$), the thermal conductivity of the sample ($\eta$) and thermal expansion of the sample ($\delta_{exp}$ (see eqn (9))). The PTIR signal was found to increase linearly with thickness of the sample up to a thickness of 1 µm. Therefore, a sample for PTIR needs to possess a significant thickness of 4–15 nm.

Fig. 9 (a) Schematic diagram of a TERS set-up in transmission mode. (b) Schematic diagrams of most commonly used TERS configurations. Bottom illumination (left), side illumination (middle) and top illumination (right). (a, b) Reprinted from open-access article ref. 240 under the terms of the Creative Commons Attribution License. (c) Mapping of photocatalytic reaction occurring at the Ag-coated TERS tip-apex using the 1142 cm$^{-1}$ peak intensity of DMAB. In the inset, a SEM image of the tip is shown. Scale bar: 100 nm. (d) Comparison of the near-field spectrum from position A in (c) with the tip in contact with the pMA/polymethylmethacrylat (PMMA) surface, its far-field spectrum (3) and far-field spectrum from position B with the tip in contact with the surface. (e) Raman mapping of the alumina-protected Ag-coated TERS tip-apex using the 1086 cm$^{-1}$ peak intensity of pMA. SEM image of the tip is shown in the inset. Scale bar: 100 nm. (f) Comparison of near-field and far-field spectra of locations A and B from (e). (1) Near-field pos. A (2–4) far-field spectra. (g) AFM topography image of a glass substrate covered with Ag nanoparticles. (h) TERS map from the dashed rectangle marked in (g), showing the variation of the 1142 cm$^{-1}$ Raman peak intensity of DMAB. (i) Near-field spectra from the positions marked in (h). (j) Intensity profile along the dotted line marked in (h), showing the spatial resolution of the TERS map. Gaussian fit to the intensity profile is shown by the dashed red curve. (c–j) Reprinted with permission from ref. 238, Copyright (2015) the Royal Society of Chemistry.
The PTIR method was enhanced by utilizing resonance enhancement in 2014. The improved method relies on the Q-fold amplification of the signal, by matching the laser repetition rate of a quantum cascade laser to the resonance frequency of the cantilever oscillation. The oscillating cantilever senses the sample expansion and the absorbed energy is transferred to the cantilever yielding in an amplification factor Q of approx. 100. This method is visualized in Fig. 11. Lu et al. utilized this specialized setup with a p-polarized pulsed mid-infrared laser to induce photo expansion of polyethylene glycol methyl ether thiol (PEG) islands adsorbed on a gold modified mica surface. By this means, the Q-factor was enhanced to around 93 and thus, the sensitivity was estimated to 30 molecules of PEG with a thickness of 2 nm. Via this method, a resolution of up to 25 nm was achieved (Fig. 11i) while even monolayers can be analyzed. Researchers have shown that polymers and self-assembled monolayers (SAMs) can be investigated via resonance enhanced-atomic force microscopy-infrared spectroscopy (RE-AFM-IR) recently, the coupling of mode synthesizing atomic force microscopy (MS-AFM) with PTIR was proposed, and vesicles inside of bacteria could be detected and analyzed in situ. This method can potentially be generalized to nanocontainers inside soft matter.

Nowadays, PTIR is superseded by infrared photoinduced force microscopy (IR-PiFM) and recently, by peak force infrared microscopy (PFIR) both methods are related to PTIR. However, IR-PiFM is different from other spectrascopically sensitive force-detection techniques as it can be operated in non-contact mode, generating high-resolution measurements in the sub-10 nm range while it can be conducted at ambient conditions without harmful contact between tip and sample, as shown in Fig. 12a. For example, Nowak et al. utilized this technique for chemical imaging of self-assembled block copolymer polystyrene-b-epoxydicyclopentadiene methacrylate (PS-b-PEDCPMA) patterns. Specifically, an incident mid-IR laser was employed to pulse at $f_m - f_1$, where $f_0$ and $f_1$ are the first and second mechanical eigenmode resonances of the cantilever. The topography of the sample was recorded by the AFM feedback system at $f_1$, and the PiFM was concurrently recorded at $f_0$ by the feedback laser position-sensitive detector and lock-in electronics. The sample was raster-scanned under the tip to generate the image. The incident light was polarized along the tip axis to maximize the signal coupling of the dipole–dipole force along the vertical direction of the cantilever vibration. High spatial resolution and chemical specificity were obtained by resolving and identifying each domain with ~40 nm pitch (Fig. 12b–i).

Similarly, PFIR is capable of chemical imaging, a collection of infrared spectra, and mechanical mapping at a spatial resolution of 10 nm. An advantage of this technique is the possibility to gather on top of chemical and topographical data also mechanical data, such as adhesion or moduli. Wang et al. showed its appliance, for example for the nanoscale phase separation in block copolymers.

2.7 AFM & ellipsometry - scanning near-field ellipsometry microscopy (SNEM)

Ellipsometry detects the changes of polarization of incident light while it is reflected from a surface. The polarization change is measured via the ellipsometry angles. These angles are related to parameters, such as thickness and the refractive index of the sample. The method is utilized to characterize...
material properties, such as composition,\textsuperscript{307} thickness (depth),\textsuperscript{308} crystalline nature,\textsuperscript{309} doping concentration,\textsuperscript{310} electrical properties\textsuperscript{311} and other material properties. AFM and ellipsometry were first combined in 2001, a scheme of such a combination is shown in Fig. 13a, to characterize concomitant optical (local refractive index) and topographical properties of thin polymer films.\textsuperscript{312} Via exploiting the electric field enhancement at a gold-coated AFM tip the signal to noise ratio (see Fig. 13b and c), as well as the resolution of the ellipsometry images, was enhanced by Tranchida et al., which was ascribed...
to lightning-rod effect and localized surface plasmons (see also TERS enhancement). The field enhancement was shown to be strongly distance dependent, denoting a significant effect at distances lower than 100 nm. They were able to visualize concomitant with the AFM and the ellipsometry nanoparticles embedded in poly(methyl methacrylate) and microphases in
microphase-separated block copolymer films (vide Fig. 13c). For the enhancement effect, a tip with a gold surface is needed. Gold garners atmospheric contaminants and therefore a steady degradation in performance is observed in SNEM as well as TERS. Cumurcu et al. proposed a protective layer of ethanethiol (self-assembled monolayer), which yields consistent and reproducible results for scanning near-field ellipsometry microscopy for at least 5 days (storage at ambient conditions). The combined SNEM method was advanced by Cumurcu et al. to a concomitant tapping mode SNEM measurement, which was applied for microphase-separated morphology of polystyrene–block–poly(2-vinylpyridine) (PS-b-P2VP) block copolymer thin films, reducing the inflicted damage originating from contact of the tip with the surface.

2.8 A combination of AFM with reflection interference contrast microscopy (RICM)

The method RICM was invented in the 1960s to study the interaction of cells with a glass substrate. It is an interferometric technique that allows the determination of the vertical distance and of the contact area between the interfaces. RICM is a label-free method (similar to IR, Raman, and ellipsometry) and can be implemented into a standard inverted microscope with little investment. A RICM setup comprises out of a monochromatic light source, an inverted microscope equipped with an anti-flex objective and a CCD camera. The light beam passes an aperture diaphragm (AD) and a field diaphragm (FD), which is positioned with respect to the sample and objective to obtain a Köhler illumination. This illumination method generates an extremely even illumination. Subsequently, the light is linear polarized, reflected by a semi-reflecting mirror and passed through a quarter wave plate, which renders the light circularly polarized. The light is transmitted and reflected by the glass substrate and the sample (i.e. a cell). The reflected light of different distances from the glass surface (i.e. membrane a few nanometers away from the glass surface) interfere with polarized light reflected directly at the glass surface, which leads to constructive or destructive interference. The interference pattern is subsequently recorded as a two-dimensional matrix of intensities known as Newton rings. Out of these rings, the distance between two surfaces can be calculated by eqn (10).

$$I(x) = I_1 + I_2 + 2\sqrt{I_1 I_2} \cos(2\theta k h(x) + \pi)$$

(10)

Here, $k = 2\pi n/\lambda$, where $\lambda$ is the wavelength of the monochromatic light, $h(x)$ is the separation distance between the two surfaces and $I_1$ and $I_2$ are the intensity of light reflected from the upper glass surface and the surface of the bead, respectively. A conceptional setup of a coupled measurement of AFM and RICM is shown in Fig. 14a.

In a combination with AFM, RICM can be a powerful tool, as it can assess the contact area of an AFM-tip with the surface/polymer membrane. Therefore, it is a pivotal technique to study inter-surface interactions. The significance of the combination was boosted by advent of soft colloidal probes in AFM measurements, as by RICM the actual contact area is accessible, which further improved the sensitivity, for example for adhesion measurements.

Typically, the position of an interface can be detected easy and precise by an AFM. Hyaluronan brushes and other soft materials, i.e. hydrogels, possess in their swollen state a soft-matter/water interface, which is difficult to locate by AFM. At this interface, an analysis of mechanical parameters (elasticity or viscosity) is difficult. Attili et al. utilized a combination of colloidal probe AFM and RICM to determine forces and concomitant the distances between a probe and an interface. The compressive mechanics of films of the polysaccharide hyaluronan that was end-grafted to a supported lipid bilayer via a biotin anchor was investigated. The compressive response of the polymer brushes was in good agreement with a theoretical model of polymer brushes. Furthermore, via RICM linear instrumental drifts of the AFM can be corrected, as well as cantilever sensitivity was obtained without additional reference measurements.

Instead of compression, adhesion of a soft colloidal probe (SCP) was investigated by Schmidt et al. The SCP was covered
with a mannose ligand, which binds under contact to a surface covered with Concanavalin A (ConA) receptors (see Fig. 14b and c). The interaction energy between the SCP and the protein surface could be evaluated as the surface area is accessible via RICM by analysis of the extent of the central circular interference minimum. A linear relationship between the mannose density and adhesion energy was found (vide Fig. 14d), excluding affinity differences between mannose units. Therefore, multivalent binding types, such as chelate and subsite, were ruled out.

2.9 AFM coupled to surface plasmon resonance (SPR)

With surface plasmon resonance (SPR) adsorption of molecules onto metal interfaces can be determined. SPR is a label-free method, possesses a high sensitivity, is able to monitor changes in adsorption in real-time, consumes low sample volumes and is a quantitative measurement. Therefore, determination of quantitative kinetic rate constants is feasible (i.e. adsorption or desorption rate constants). In SPR the Kretschmann configuration is often utilized, which is shown in Fig. 15a. The Kretschmann configuration comprises of a thin metal film (silver or gold) at the interface of two dielectric media. A laser beam is focused onto a prism with refractive index \( n_1 \). The light is, dependent on the angle of incident, either reflected or adsorbed (resonance angle). The resonance angle changes upon the refractive index of the solution of interest, for example by adsorption. For the measurement, the solution of interest needs to possess a lower refractive index \( n_2 \). The surface plasmon resonance angle shifts, which is originating from the change in refractive index, is utilized to determine the quantitative adsorption of molecules. SPR and AFM were already combined in 1995 by Chen et al. and Shakesheff et al. As the two systems are geometric complementary (AFM measured from the top of the sample, whereas SPR measures from bottom) a combination of these two methods is fairly easy. The time resolution of the SPR together with the high sensitivity can substitute in a combined AFM-SPR measurement the lack of time resolution (for most AFM equipment) of the AFM. Early studies have analyzed the degradation of biodegradable polymer films on silver. The combination can make use of synergy of both capabilities, as AFM can determine
Fig. 15 (a) Instrumental configuration for AFM + SPR. Reprinted with permission from ref. 52 Copyright (2009) Royal Society of Chemistry. (b) Time dependence of SPR angle shift during degradation of a poly(orthoester) (POE) film exposed to flowing (1 ml s\(^{-1}\)) acidic solution (pH 3.5). The arrows indicate the acquisition of corresponding scanning force microscopy (SFM) scans (c) at the time \(t = 0\) min (c-a), \(t = 15\) min (c-b), \(t = 29\) min (c-c), \(t = 39\) min (c-d), \(t = 44\) min (c-e), and \(t = 49\) min (c-f). (b, c) Reprinted with permission from ref. 334 Copyright (1996) AIP Publishing LLC.

3. Combination of AFM with nonoptical surface sensitive methods

3.1 Combination of AFM with Kelvin method – Kelvin probe force microscopy (KPFM)

By rendering the AFM tip and the sample conductive, the work function or surface potential can be obtained with a high lateral resolution, which can be lower than 10 nm.\(^{335}\) The method is commonly denoted as Kelvin probe force microscopy (KPFM) and was first introduced in 1991 by Nonnenmacher et al.\(^{336}\) KPFM measures the contact potential difference (CPD) of a conductive AFM tip and a conductive sample. CPD is defined by the work functions of the tip (\(\Phi_{\text{tip}}\)) and the sample (\(\Phi_{\text{sample}}\)) and the elementary charge (\(e\)).

\[
V_{\text{CPD}} = \frac{\Phi_{\text{sample}}}{e} - \frac{\Phi_{\text{tip}}}{e} = \frac{\Delta \Phi}{e} \tag{11}
\]

By applying both, an AC (\(V_{\text{AC}}\) also \(U_{\text{AC}}\)) and a DC (\(V_{\text{DC}}\) also \(U_{\text{DC}}\)) voltage to the AFM tip, the work function of the sample is assessed. Here, the DC voltage repeals the CPD difference between tip and sample surface, which is oscillated due to the applied AC voltage. The cantilever oscillates at \(a \sin(\omega t)\) (sinusoidal excitation signal). \(a\) denotes the amplitude and \(\omega\) for the frequency of the sinusoidal electrical signal. The feedback controller C compensates for the surface potential \(\Phi\) indicated by \(+ + + +\) by adjusting a DC (bias) voltage \(U_{\text{DC}}\), as shown in Fig. 16a.\(^{337}\) As a consequence of these applied signals, the resulting force has three contributions, two oscillatory terms \(\omega\) and \(2\omega\) and a bias, which contributes to the topographical signal. The contact potential difference can be obtained by a lock-in technique by tuning the bias voltage \(U_{\text{DC}}\) to a value, which nulls the oscillating force signal (\(\omega\)). The contact potential difference is this needed bias voltage.

The surface potential can be determined by at least 4 methods. Here, the KPFM is the most versatile and possesses distinct advantages over standard Kelvin probe (KP), photoemission spectroscopy (PES) and scanning electron microscopy (SEM). The measurement principle of KP and KPFM is similar. The energy resolution of KP method is slightly better compared to KPFM, but KP method relies on averaging over the whole sample, indicating no or low lateral resolution is obtainable. Via PES both, lateral resolution of approximately 100 nm and 20 meV energy resolution can be obtained.\(^{339}\) However, KPFM possesses enhanced lateral and energy resolution. However, for a sample surface containing adsorbents, KPFM cannot distinguish between surface band bending and surface dipoles created by adsorbents from the sample surface.\(^{340}\) PES yields in the spectral distribution of the surface potential, which can be utilized in a comparative approach to determine band bending and surface dipole contributions, independently.\(^{340}\) A qualitative measure of the surface potential can be obtained with a lateral resolution of approximately 70 nm by SEM via electron beam induced current.\(^{341}\) KPFM has an energy resolution of 5–20 meV and a lateral resolution of 10 nm or better,\(^{335}\) depending on the utilized measurement mode.
Typically, a KPFM experiment is conducted in either an amplitude modulation mode (AM) or frequency modulation mode (FM). Here, FM-KPFM is considered the method with higher lateral resolution (up to sub-nanometer), whereas AM-KPFM possesses a higher energy resolution of up to 5 meV. The enhanced $V_{\text{CPD}}$ precision can be related to a higher signal-to-noise ratio originating from the resonance peak of the cantilever, whereas in FM mode the $V_{\text{CPD}}$ is determined by FM demodulator, which increases the noise in a measurement.

Ongoing research is devoted to enhancing the time resolution, because the scan speed of FM mode is slow and AM mode measurements are burdened with artifacts, such as the stray capacitance effect and interfering signals, leading to topographical coupling. Several approaches try to couple the lateral resolution and reproducibility of FM mode KPFM with enhanced time resolution similar to AM mode KPFM, such as time-resolved electrostatic force microscopy, pump-probe KPFM, general acquisition mode, open loop (OL) KPFM and Heterodyne (H) KPFM. For example, H-KPFM improved the scan rate while maintaining the spatial resolution and voltage sensitivity comparable to FM-KPFM. Furthermore, it is not susceptible to artifacts such as stray capacitance (AM mode), topographical oscillation (FM mode) and AC inductive coupling (AM mode) artifacts. However, artifacts originating from collisions with the surface persist.

KPFM is applied for characterization of metal and semiconductor surfaces, organic films and biological membranes. Surface potential mapping is utilized for distinguishing carbon from the alloying elements, such as Al, Zn and Mg, as the surface potential difference is relatively small for carbon (similar work function as the tip (Pt)), as is illustrated in Fig. 16b–e. In contrast, the potential difference between the metals and tip are high. For example, Jaim et al. utilized KPFM to analyze the difference between Al-6061 cv 3% and Al-6061 and substantiated the presence and the ribbon networks of carbon embedded in the Al-matrix of Al-6061 cv 3%.
observed a correlation of the dark regions in the AFM phase image (Fig. 16b) and KPFM image (Fig. 16c), which was ascribed to carbon as it possesses a lower work function compared to the Al-matrix surface potential. Consequently, Al-6061 does not show this correlation between AFM phase and KPFM image, which appears to possess a rather homogeneous CPD. Another common area of application of KPFM is the analysis of semiconductors. Here, the KPFM method is sensitive enough to determine the dopant concentration in the range of $10^{14}$ cm$^{-3}$ to $10^{19}$ cm$^{-3}$. However, the contact potential difference is altered by surface defects, exploitable for detecting of defects. By illumination with a sub-bandgap laser, band bending is reduced and higher contrast in CPD in conjunction with reduced influence on surface defect states is achieved.

KPFM can be applied for Langmuir–Blodgett films of organic molecules on water (subphase) to assess the packing of the organic molecules at varying surface pressure by means of the CPD. Furthermore, KPFM can be utilized to ascertain charge transfer from Pt adsorbates to TiO$_2$ surface and analysis of charge separation for the benchmark of organic solar cells, which for example consist of poly(3-hexylthiophene) (P3HT)/fullerene (C$_{60}$) acid-methyl ester (PCBM). An interesting application, which also shows the high lateral resolution and sensitivity, is the analysis of quantum size effects (QSE) proposed by Späth et al. In contrast to other techniques, KPFM was able to directly address the single digit nanometer height of single Pb islands on Si while simultaneously assessing the local work function (see Fig. 17). Yamagishi et al. utilized KPFM to visualize trapped charges in organic thin-film transistor (OTFT) channels. KPFM was utilized in the biological area to examine the effects of surface potential on microbial adhesion on various metals. The surface potential of the microbial was dependent on adsorbents and was linked with changes in cellular metabolism and motility.

3.2 AFM combined with quartz crystal microbalance (QCM)

QCM is a method to detect and quantify change of the mass by a shift in the frequency of vibration of a piezoelectric device. The frequency shift ($\Delta F$, eqn (12)) of the resonator is dependent on the fundamental frequency of quartz resonator ($F_0$), change of mass on the surface of quartz resonator ($\Delta m$) and the vibrating surface area ($A$).

$$\Delta F = -2.3 \times 10^{6} F_0 \frac{\Delta m}{A}$$

In addition to the detection of mass change, it may provide information about the conformation of molecules adsorbed to the surface by damping of the oscillation (amplitude). The latter information is often hard to come by, as changes in shape cannot directly be related to a QCM response. On the other hand, it is feasible to analyze changes in shape by AFM. Therefore, it is conducive for analysis of QCM data. For a combined measurement, the oscillation amplitude has to be lower than the desired resolution of the AFM experiment. The first combination was reported in 1998 by Iwata et al. and was used to evaluate the morphology and mass change at the liquid/solid interface during the electrodeposition of Ag on a Pt thin film. For electrochemistry purposes, a specialized three-electrode cell was utilized, comprising of an Au coated quartz crystal working electrode (WE), Ag wire reference electrode (RE), and Zn foil counter electrode (CE) (see Fig. 18a). Such a setup was successful in performing in situ electrochemistry, as shown in Fig. 18b–d. For example, Smith et al. were able to confirm that the growth mechanism of electrodeposited Zn resembles a 3D progressive model. Thus, this hybrid method imparts a realistic prospect of understanding of electrochemical nucleation and growth, which may be transferable to other issues outside electrochemistry. Most recently, Kelvin probe microscopy was annexed to an AFM-QCM combination to improve the versatility. This approach was utilized to measure the response of tin oxide-based sensors and determine during adsorption of analyte in situ the work function of the sensor nanomaterial (i.e. SnO$_2$, Pd-doped SnO$_2$, and bromocresol purple-doped HfO$_2$).

3.3 AFM combined with thermal imaging – scanning thermal microscopy (SThM)

Scanning thermal microscopy (SThM) maps the local temperature and thermal conductivity of interfaces. SThM allows thermal measurements at the nano-scale. Besides temperature and energy transport, processes involving the exchange of energy and entropy with the surroundings are feasible, such as thermal properties of materials, thermal conductivity, heat capacity, glass transition temperature, latent heat, enthalpy, etc.
In 1986, shortly after the scanning tunneling microscope was invented, Williams and Wickramasinghe reported a nanoscale measurement exploiting thermal phenomena. Several scanning thermal microscopes were established, which are mainly based on atomic force microscopy. Here, the combined system with the AFM diversifies the applicability, for example by performing measurements as a function of the tip-sample force and distance or by varying sensor types and geometries. The working principle of SThM is dependent on the utilized thermal method. The methods can be classified according to the temperature-dependent mechanism into either (a) thermovoltage, (b) change in electrical resistance, (c) fluorescence or (d) thermal expansion. However, these methods are still under rapid development and other techniques have been proposed, for example a method based on simultaneous registration of the static and the dynamic electrical resistance of the probe driven by the sum of DC and AC currents, which is suitable for thin films deposited on thick substrates.

Thermovoltage-based measurements can be conducted either in contact or in non-contact mode. Crucial, but also limiting its applicability is the need for an electrically conducting surface of the sample. The working principle of thermovoltage methods can be tunneling thermometry or the point-contact thermocouple method. As probes in thermovoltage-based methods, thermocouples (see Fig. 19c) and Schottky diode are utilized. Accessible via these methods are the temperature and the thermal conductivity at a minuscule surface area. The lateral resolution utilizing a thermovoltage method is in the nm range and both the lateral resolution and probe thermal time constant of an experiment was substantial enhanced by miniaturization of the cantilever, the tip and the junction at the tip. However, these methods are per se not quantitative due to the dependence between temperature rise measured locally on the size of the heated area (heat transfer also via gas), as shown in Fig. 19b. Vacuum conditions (below 0.1 Pa) with an active thermal feedback scheme allows maintaining the tip temperature equal to the sample surface temperature.
Nevertheless, null-point SThM (NP-SThM) and the previously mentioned ultra-high vacuum method circumvent this limitation, and outstanding thermal (~15 mK) and spatial (~10 nm) resolutions were obtained (see also Fig. 19d–f). Thermal conductivity is probed via the two omega (2ω) method. To this end, an AC current at a frequency ω is applied to the thermoelectric probe. The current passing from the SThM probe to the sample surface via the thermocouple junction generates heat at a frequency of 2ω, which leads to an oscillation of the junction temperature at 2ω and the amplitude of the 2ω signal from the thermocouple junction is monitored. Recently, a 2ω method was proposed utilizing...
a micro-thermocouple probe placed on a Quartz Tuning Fork (QTF), which circumvents the imprecise surface detection by optical deflection methods. Nevertheless, some artifacts persist during the measurement, for example Kim et al. observed a different temperature profile during the measurement of a heated Pt line in slow and fast scan mode, which was assigned to differences in contact area between tip and sample, resulting in a change in thermal resistance between the tip and the sample, as shown in Fig. 19e and f.

(b) The change in electrical resistance can be utilized to determine the temperature at a small region on a sample. A heater with frequency $\omega$ heats the sample at $2\omega$ frequency, similar to the $2\omega$ method. The temperature oscillation at a frequency of $2\omega$ results in an oscillation of the resistance of the second probe, which is thermal sensor, at $2\omega$.

(c) The fluorescence intensity depends strongly on the temperature, as the emitted intensity $I_{em}$ is proportional to the population of excited states. By monitoring the fluorescence intensity at a given frequency, the temperature change can be derived from the change in fluorescence intensity. To enhance this approach, Aigouy et al. proposed gluing a fluorescent particle to the tip apex, which is afterward utilized for the local temperature measurement.

(d) Thermal expansion (thermoacoustic effect) can be utilized to measure the increase of temperature as thermal expansion coefficient is usually in a range close to $10^{-5}$ m K$^{-1}$ and the dilation can be measured accurately via AFM. The sample can be either heated by Joule heating or optically, similar to AFM-IR.

Several approaches to enhance the lateral and thermal resolution have been investigated. In the beginning, in SThM

![Fig. 20](image-url)
a Wollaston wire probe with a temperature coefficient \( a = 0.00166 \, \text{K}^{-1} \) and time response of approximately 200 ms (in air) was utilized, which limits the lateral resolution of an experiment.\(^{394-396}\) Smaller metallic probes attached to cantilevers with a low spring constant (0.35 N m\(^{-1}\)) and a tip radius of around 50 nm improved the lateral resolution.\(^{396-397}\) Furthermore, this probe enhanced the time response to a few tens of ms while maintaining a similar temperature coefficient as the Wollaston wire.\(^{398}\) Recently, high thermal conductivity nanowires (NW) attached to a tip apex were proposed to address the low efficiency of thermal coupling in SThM, approach, while maintaining the lateral resolution.\(^{399}\) It has to be mentioned that the tip-sample heat transfer is crucial for the lateral resolution. Menges et al. developed a method, probing a time-dependent and a time-averaged heat flux signal between a self-heated scanning probe sensor and a temperature-modulated sample, permitting the elimination of tip-sample contact-related artifacts, a major step of SThM towards nanoscale thermometry.\(^{400}\)

As stated previously, SThM can measure temperature (passive mode), thermal conductivity (active mode) and local phase-change transition (active mode) of a sample. The measurement of temperature is exploited for point studies and mappings of the amplitude of the steady periodic temperature field. It was utilized for the characterization of the temperature profile measurements of a PN thermoelectric couple and hot-spots in integrated circuits.\(^ {401,402}\) Similar to KPFM, SThM in thermal mode can prove useful for failure localization and analysis of integrated circuits.\(^ {403-405}\) By the aforementioned smaller probes, heat dissipation, thermal conductivity or transport pathways in multiwall carbon nanotubes (MWCNs), single wall carbon nanotubes (SWCNs), graphene oxide (see Fig. 20a and b)\(^ {405}\) and various other nanocomponents was determined.\(^ {406}\) Furthermore, Joule self-heated nanomaterials, such as graphene nanoribbons (GNRs),\(^ {407}\) silicon nanowire, nanowire diode and nanoscale metal interconnect structures (see Fig. 20c–h),\(^ {408}\) and photo-induced heating\(^ {409}\) were analyzed via this method. The thermal conductivity of materials was probed at the level of the thermal diffusion.\(^ {410}\) Subsurface volumes for bulk ZnO and simple binary intermetallic clathrates (Ba\(_4\)Si\(_{16}\)), porous bulks,\(^ {411-413}\) mesoporous bulks\(^ {414}\) and thin films of submicrometric thickness.\(^ {415}\) Recently, SThM was utilized to determine the penetration depth of an adhesive in wood (subsurface imaging).\(^ {416}\) Via the measurement of the heat conductivity, the phase transition between martensite-austenite of NiTi microstructures was accessible.\(^ {416}\) Furthermore, the glass transition \( T_g \) and melting temperature \( T_m \) of polymers or polymer blends at submicron scale is accessible (method is also named nano-TA).\(^ {418}\)

4. Conclusion and future aspects

The combination of several orthogonal techniques is a fertile research field. Especially, hybrid analysis tools comprising out of two complementary techniques, which can compensate for their intrinsic weaknesses, are employed and refined while novel approaches are investigated in recent years. All these attempts to design hybrid analysis tools with nanometer resolution are driven by the search for advanced means to analyze and characterize new nanomaterials with high sensitivity and spatial resolution as well as to analyze processes occurring at the nanoscale, be it transport processes in biological samples or electronic processes at metal interfaces. Therefore, a strong emphasis was on combinations of optical methods, which are impeded by its low resolution, and AFM. Here, tremendous effort has been devoted to the improvement of resolution, signal-to-noise ratio and alignment/drift of the AFM. Furthermore, novel methods, such as SNEM and PTIR were actively developed, which yielded in the development of IR-PiFM, a noninvasive method of combined AFM and IR measurement with an unprecedentedly high optical resolution when compared with other IR measurement techniques. Still, some issues remain unsolved, for instance, the lifetime of the tip-apex in SNEM, PTIR and TERS is short, which results in a loss of signal after a few hours. Nonetheless, these tip-enhanced methods are invaluable nowadays as they provide chemical fingerprints or chemical structures at sub-diffraction resolution. Combinations out of AFM and an optical microscope can be advanced by adding further measurement techniques, such as fluorescence spectroscopy, fluorescence anisotropy and fluorescence lifetime. Although commercial solutions, at least for FLIM in combination with AFM are present, their alignment and computerized control still lack. These combined methods based on optical measurement techniques were mainly but not exclusively applied to biological samples (e.g. lipids, proteins, cells, viruses, particles, or biofilms), although these techniques also possess applications in material science and surface science (see surface nanobubbles).

In contrast, the non-optical techniques were predominantly utilized in applications related to material science and engineering (e.g. semiconductors and nanomaterials). Surface analysis techniques, relying on non-optical techniques, have emerged and effort has been devoted to these surface analysis techniques (KPFM and SThM) to improve their lateral resolution as well as their time resolution and precision. Still, resolution of these techniques is lower than for AFM on its own. Here, a variation of tip-tip geometry and tip material has shown to enhance these parameters. Further advancement would benefit material science and engineering, as these methods are utilized to examine the properties of semiconductors for computers, which are presently undergoing miniaturization.

Some techniques, like QCM, SPR, FCS and RICM, are rarely combined with the AFM, which can be related to different acquisition times, issues with alignment and/or lack of data interpretation. However, these hybrid methods potentially give insight into processes appearing at interfaces at a molecular level. For example, despite the scarce application of RICM in literature, it has the potential to become a vital technique for determination of the actual contact area, which is important for adhesion measurements of soft colloidal probes.
In spite of the fact that most of the combined techniques are still under development and improvement, and equipment optimization is pending, hybrid techniques are highly important in the areas of biology, surface science (physical chemistry) and material science. Subsequently, Table 1 shows a comprehensive list of all major combined techniques mentioned in this review, together with their typical resolution, the field of application, advantages, and drawbacks, serving as a decision guidance for the interested reader. We anticipate that this review will provide a comprehensive overview of the hybrid measurement techniques based on the combination of surface sensitive techniques with the atomic force microscope. Besides, it will impart knowledge of the field of application of a specific combination in conjunction with its intrinsic advantages and limitations and thus serve as a viable tool for deciding on the most beneficial measurement method.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

We acknowledge the National Natural Science Foundation of China (21674064 and 21404072) for financial support of this work. We thank Lili Wang for fruitful discussions.

| Resolution | Samples | Measurant | Advantages | disadvantages |
|------------|---------|-----------|------------|---------------|
| SNOM, s-SNOM | Lateral ≈ 30 nm, axial ≈ 10 nm | Membranes, carbon nanotubes, polymers, biological samples | Refractive index, reflectivity, transparency, polarization, fluorescence... | High resolution, high sensitivity (single molecule) | Low working distance, scan time, analysis difficult, artifacts |
| AFM-fl. microscopy | Lateral ≈ see CLSMb,c, axial ≈ 2000 nmb,c | Pre. biological | Intensity, location, movement | Very fast acquisition time | Low axial resolution, label required |
| AFM-TIRF | Lateral ≈ see CLSMb,c, axial ≈ 20–100 nm,b,c | Pre. biological | Intensity, location, movement | Very fast acquisition time, high sensitivity, selective excitation at interface | Limited to the interface (around 100 nm), label required |
| AFM-CLSM | Lateral ≈ 200 nm,b,c, axial ≈ 500 nm,b,c | Pre. biological | Intensity, location, movement | Fast acquisition, optical slicing, high sensitivity | Low axial resolution, label required |
| AFM-FCS | See AFM-CLSM, volume ≈ 1 fl | Pre. membranes | Concentration, size diffusion coefficient | Correlate diffusion with topography, high sensitivity | Drift in AFM, artifacts, label required |
| AFM-FLIM | See AFM-CLSMb,c | Pre. biological, surface analysis | Intensity, fl. lifetime, movement/diffusion | Modulation effects, fast, multidimensional | Proximity of tip can alter lifetimes, artifacts label required |
| AFM-STED | Lateral ≈ 20 nm,b,c, axial ≈ 100 nm,b,c | Pre. biological | Intensity, movement/diffusion | High resolution, high sensitivity | Bleaching, specific dyes, special label required |
| PTIR/RE-AFM-IR | Lateral 25 nm/10 nm | Biological, thin films | IR spectrum | Chemical ident. and fingerprint, label-free | Tip lifetime limited, contact mode required |
| IR-PfFM, PfIR | See PTIR | Biological, thin films, monolayers, polymers | IR spectrum | Chemical ident. and fingerprint, NC mode | Tip lifetime limited |
| TERS | Lateral 1–20 nm | Biological, thin films, polymers | Raman spectrum | Chemical ident. and fingerprint, label-free | Tip lifetime limited |
| KPFM | Better than 10 nm, 5–20 meV | Semiconductor, organic films, metals | Contact potential difference | High resolution, defects detectable, label-free | Artifacts |
| SNEM | Lateral ≤ 2/10 | Semiconductor, biology, polymers | Complex refractive index, thickness | Composition accessible, label-free | Tip lifetime limited |
| AFM-RICM | Lateral nanometer, axial nanometer | Soft interfaces, soft probes | Contact surface area, distance | Fast and real time, label-free | Limited to distance and contact area |
| AFM-QCM | Dependent on the size of QCM crystalb | Adsorption of particles, polymers, proteins... | Frequency shift, adsorbed mass | High accuracy, real time, label-free | Analysis difficult, scarce |
| AFM-SPR | Lateral 600 nm | Adsorption/binding of molecules/proteins | Refractive index, adsorbed mass | Fast and real time, label-free | Thin metal surface needed |
| SThM (also nano-TA) | Lateral up to 10 nm, heating ~100 nm, up to 15 mK | Semiconductors, metals, nanocomposite | Temperature, thermal conductivity, phase transitions | Conductivity needed, several heat transport pathwaysa | |

a For thermovoltage measurements. b Resolution of the complementary technique, resolution of AFM remains sub nm (lateral) and sub Angstrom (axial). c Tip enhancement effects may apply, pre. = predominant, fl. = fluorescence, ident. = identification NC = noncontact.
Near-Field Characterization of Micro/Nano-Scale Fluid Flows

S. Liang, Y. Li, J. Yang, J. Zhang, Y. Liu, Z. Liu, C. He and X. Zhou, *Adv. Sci.*, 2017, 4, 1700028.

D. Zhu, S. Handschu-Wang and X. Zhou, *J. Mater. Chem. A*, 2017, 5, 16467–16497.

M. Bohrer, M. Schweitzer, R. Nürnberger and B. Weinberger, *Proc. SPIE*, 2015, 9636, 963609.

P. Ye, H. Yu and M. Houchmandi, *BMC Oral Health*, 2016, 16, 1–9.

S. Bosi, R. Rauti, J. Laishram, A. Turco, D. Lonardoni, T. Nieus, M. Prato, D. Scaini and L. Ballerini, *Sci. Rep.*, 2015, 5, 9562.

M. Maglione and S. J. Sigrist, *Nat. Neurosci.*, 2013, 16, 790–797.

E. Abbe, *Archiv für Mikroskopische Anatomie*, 1873, 9, 413–420.

S. Schnorrer, T. Grotjohann, G. Vorbruggen, A. Herzig, S. W. Hell and S. Jakobs, *eLife*, 2016, 5, e15567.

P. Hoyer, G. de Medeiros, B. Balazs, N. Norlin, C. Besir, J. Hanne, H. G. Krausslich, J. Engelhardt, S. J. Sahl, S. W. Hell and L. Hufnagel, *Proc. Natl. Acad. Sci. U. S. A.*, 2016, 113, 3442–3446.

S. W. Hell, S. J. Sahl, M. Bates, X. W. Zhuang, R. Heintzmann, M. J. Booth, J. Bewersdorf, G. Shtengel, H. Hess, P. Tinnefeld, A. Honigmann, S. Jakobs, I. Testa, L. Cognet, B. Lounis, H. Ewers, S. J. Davis, C. Egginger, D. Klennerman, K. I. Willig, G. Viciodomini, M. Castello, A. Diaspro and T. Cordes, *J. Phys. D: Appl. Phys.*, 2015, 48, 443001.

S. W. Hell, *Science*, 2007, 316, 1153–1158.

S. W. Hell and J. Wichmann, *Opt. Lett.*, 1994, 19, 780–782.

M. J. Broadhead, M. H. Horrocks, F. Zhu, L. Muresan, R. Benavides-Piccione, J. DeFelipe, D. Fricker, M. V. Kopanitsa, R. R. Duncan, D. Klennerman, N. H. Komiyama, S. F. Lee and S. G. N. Grant, *Sci. Rep.*, 2016, 6, 24626.

A. Yildiz and P. R. Selvin, *Acc. Chem. Res.*, 2005, 38, 574–582.

D. Kim, T. J. Deerinck, Y. M. Sigal, H. P. Babcock, M. H. Ellisman and X. Zhuang, *PLoS One*, 2015, 10, e0124581.

D. Wildanger, B. R. Patton, H. Schill, L. Marseglia, J. P. Hadden, S. Knauer, A. Schöne, J. G. Rarity, J. L. O’Brien, S. W. Hell and J. M. Smith, *Adv. Mater.*, 2012, 24, 309–313.

C. Egginger, K. I. Willig and F. J. Barrantes, *J. Neurochem.*, 2013, 126, 203–212.

B. Harke, J. Keller and S. W. Hell, *Opt. Express*, 2008, 16, 4154–4162.

M. Dyba and S. W. Hell, *Phys. Rev. Lett.*, 2002, 88, 163901.

J. Bücker, D. Wildanger, G. Viciodomini, L. Kastrup and S. W. Hell, *Opt. Express*, 2011, 19, 3130–3143.

E. Auksorius, B. R. Boruah, C. Dunsby, P. M. P. Lanigan, G. Kennedy, M. A. A. Neil and P. M. W. French, *Opt. Lett.*, 2008, 33, 113–115.

M. Fernandez-Suarez and A. Y. Ting, *Nat. Rev. Mol. Cell Biol.*, 2008, 9, 929–943.

S. Ghosh, H. Remita, L. Ramos, A. Dazzi, A. Deniset-Besseau, P. Beaunier, F. Goubard, P.-H. Aubert, F. Brisset and S. Remita, *New J. Chem.*, 2014, 38, 1106–1115.

G. Hwang and O. Kwon, *Nanoscale*, 2016, 8, 5280–5290.

T. Tai, O. Karácsony, V. Bocharova, G. J. Van Berkel and V. Kertesz, *Anal. Chem.*, 2016, 88, 2864–2870.

S. Moreno Flores and J. L. Toca-Herrera, *Nanoscale*, 2009, 1, 40–49.

J. M. Gerton, L. A. Wade, G. A. Lessard, Z. Ma and S. R. Quake, *Phys. Rev. Lett.*, 2004, 93, 180801.

V. Walhorn, O. Schulz, C. Pelargus, D. Anselmetti and R. Ros, *Proc. SPIE*, 2007, 6444, 644406.

Y. Ebenstein, T. Mokari and U. Banin, *J. Phys. Chem. B*, 2004, 108, 93–99.

Z. Y. Ma, J. M. Gerton, L. A. Wade and S. R. Quake, *Phys. Rev. Lett.*, 2006, 97, 260801–260804.

E. Yoskovitz, D. Onor, I. Shewky and U. Banin, *J. Phys. Chem. C*, 2008, 112, 16306–16311.

O. Schulz, Z. Zhao, A. Ward, M. König, F. Koerberling, Y. Liu, J. Enderlein, H. Yan and R. Ros, *Opt. Nanoscopy*, 2013, 2, 1.

J. L. Garrett and J. N. Munday, *Nanotechnology*, 2016, 27, 245705.

E. Birkenhauer and S. Neethirajan, *J. Visualized Exp.*, 2014, 93, e52327.

K. Kim, W. Jeong, W. Lee and P. Reddy, *ACS Nano*, 2012, 6, 4248–4257.

S. Sadewasser, T. Glatzel, M. Rusu, A. Jäger-Waldau and M. C. Lux-Steiner, *Appl. Phys. Lett.*, 2002, 80, 2979–2981.

P. Eaton and P. West, *Atomic force microscopy*, Oxford University Press Inc., New York, 2010.

H. Schönherr and G. J. Vancso, *Scanning Force Microscopy of Polymers*, Springer-Verlag, Berlin-Heidelberg, 2010.

J. Zhong and J. Yan, *RSC Adv.*, 2016, 6, 1103–1121.

D. P. Allison, N. P. Mortensen, C. J. Sullivan and M. J. Doktycz, *Wiley Interdiscip. Rev.: Nanomed. Nanobiotechnol.*, 2010, 2, 618–634.

Y. F. Dufrêne, T. Ando, R. García, D. Alsteens, D. Martinez-Martin, A. Engel, C. Gerber and D. J. Muller, *Nat. Nanotechnol.*, 2017, 12, 295–307.

W. B. Amos and J. G. White, *Biol. Cell.*, 2003, 95, 335–342.

A. Ostrowski, D. Nordmeyer, A. Boreham, C. Holzhausen, L. Mundhenk, C. Graf, M. C. Meinke, A. Vogt, S. Hadam, J. Lademann, E. Rühl, U. Alexiev and A. D. Gruber, *Beilstein J. Nanotechnol.*, 2015, 6, 263–280.

M. Minsky, *Microscopy Apparatus*, *US Pat.*, 3031.467, 1957.

I. Schermelleh, R. Heintzmann and H. Leonhardt, *J. Cell Biol.*, 2010, 190, 165–175.

K. D. Kimh, *Near-Field Characterization of Micro/Nano-Scale Fluid Flows*, Springer, Berlin-Heidelberg, 2011.

M. Grossi, M. Morgunova, S. Cheung, D. Scholz, E. Conroy, M. Terrile, A. Panarella, J. C. Simpson, W. M. Gallagher and D. F. O’Shea, *Nat. Commun.*, 2016, 7, 10855.

S. Liang, Y. Li, J. Yang, J. Zhang, C. He, Y. Liu and X. Zhou, *Adv. Mater. Technol.*, 2016, 1, 1600117.

S. Liang, Y. Li, Y. Chen, J. Yang, T. Zhu, D. Zhu, C. He, Y. Liu, S. Handschu-Wang and X. Zhou, *J. Mater. Chem. C*, 2017, 5, 1586–1590.
200 F. Zenhausern, M. P. O’Boyle and H. K. Wickramasinghe, Appl. Phys. Lett., 1994, 65, 1623.
201 Y. Martin, F. Zenhausern and H. K. Wickramasinghe, Appl. Phys. Lett., 1996, 68, 2475.
202 A. Kramer, W. Trabesinger, B. Hecht and U. P. Wild, Appl. Phys. Lett., 2002, 80, 1652.
203 N. Hayazawa, Y. Inouye and S. Kawata, J. Microsc., 1999, 194, 472–476.
204 J. Azoulay, A. Débarre, A. Richard and P. Tchénio, J. Microsc., 1999, 194, 486.
205 A. Hartschuh, E. J. Sánchez, X. S. Xie and L. Novotny, Phys. Rev. Lett., 2003, 90, 095503.
206 T. Ichimura, N. Hayazawa, M. Hashimoto, Y. Inouye and S. Kawata, Phys. Rev. Lett., 2004, 92, 220801.
207 H. G. Frey, J. Paskarbeight and D. Anselmetti, Appl. Phys. Lett., 2009, 94, 241116.
208 N. Behr and M. Raschke, J. Phys. Chem. C, 2008, 112, 3766–3773.
209 W.-S. Chang, S. Bauerdick and M. S. Jeong, Ultramicroscopy, 2008, 108, 1070–1075.
210 Z. Shi, X. Hong, H. A. Bechtel, B. Zeng, M. C. Martin, K. Watanabe, T. Taniguchi, Y.-R. Shen and F. Wang, Nat. Photonics, 2015, 9, 315–519.
211 B. Pollard, E. A. Muller, K. Hinrichs and M. B. Raschke, Nat. Commun., 2014, 5, 3587.
212 S. A. Donges, O. Khatib, B. T. O’Callahan, J. M. Atkin, J. H. Park, D. Cobden and M. B. Raschke, Nano Lett., 2016, 16, 3029–3035.
213 N. El-Kork, P. Moretti, B. Jacquier, F. Lei and M. Ismail, J. Nanomater., 2016, 4089260.
214 L. Andolfi, E. Trevisan, B. Troian, S. Prato, R. Boscolu, E. Giolo, S. Luppi, M. Martinelli, G. Ricci and M. Zweyer, J. Nanobiotechnol., 2015, 13, 2.
215 Y. De Wilde and P. A. Lemoine, AIP Conf. Proc., 2007, 931, 43–52.
216 R. Gaifulina, A. T. Maher, C. Kendall, J. Nelson, M. Rodriguez-Justo, K. Lau and G. M. Thomas, Int. J. Exp. Pathol., 2016, 97, 337–350.
217 A. K. Meher and Y.-C. Chen, Anal. Chem., 2016, 88, 9151–9157.
218 K. Luo, Y. D. Xiang, H. M. Wang, L. Xiang and Z. H. Luo, J. Mater. Sci. Technol., 2016, 32, 733–737.
219 C. S. Casari, C. S. Giannuzzi and V. Russo, Carbon, 2016, 104, 190–195.
220 T. Kavinkumar and S. Manivannan, J. Mater. Sci. Technol., 2016, 32, 626–632.
221 W. Miranda, S. S. Coutinho, M. S. Tavares, E. Moreira and D. L. Azevedo, J. Mol. Struct., 2016, 1122, 299–308.
222 P. K. Chu and L. Li, Mater. Chem. Phys., 2006, 96, 253–277.
223 E. V. Efremov, F. Ariese and C. Gooijer, Anal. Chim. Acta, 2008, 606, 119–134.
224 S. Bonhommeau, D. Talaga, J. Hunel, C. Cullin and S. Lecomte, Angew. Chem., 2017, 129, 1797–1800.
225 P. C. Gutiérrez-Neira, F. Aguillo-Rueda, A. Climent-Font and C. Garrido, Vib. Spectrosc., 2013, 69, 13–20.
226 S. Boyd, M. F. Bertino and S. J. Seashols, Forensic Sci. Int., 2011, 208, 124–128.
227 G. Barone, D. Bersani, J. Jehlicka, P. P. Lottici, P. Mazzoleni, S. Raneri, P. Vandenabeele, C. Di Giacomo and G. Larina, J. Raman Spectrosc., 2015, 46, 989–995.
228 M. N. Kinalwa, E. W. Blanch and A. J. Doig, Anal. Chem., 2010, 82, 6347–6349.
229 S. Signorelli, S. Cannistraro and A. R. Bizzarri, Appl. Spectrosc., 2016, 71, 823–832.
230 H. J. Butler, L. Ashton, B. Bird, G. Cinque, K. Curtis, J. Dorney, K. Esmonde-White, N. J. Fullwood, B. Gardner, P. L. Martin-Hirsch, M. J. Walsh, M. R. McAnish, N. Stone and F. L. Martin, Nat. Protoc., 2016, 11, 664–687.
231 N. Kumar, M. M. Drozdz, H. Jiang, M. D. Santos and D. J. Vaux, Chem. Commun., 2017, 53, 2451–2454.
232 P. Mukherjee, S. J. Lim, T. P. Wrobel, R. Bhargava and A. M. Smith, J. Am. Chem. Soc., 2016, 138, 10887–10896.
233 T. Iwasaki, T. Zelai, S. Ye, Y. Tsuchiya, H. M. H. Chong and H. Mizuta, Carbon, 2017, 111, 67–73.
234 A. Paudel, D. Rajjada and J. Rantanen, Adv. Drug Delivery Rev., 2015, 89, 3–20.
235 L. S. Lawson and J. D. Rodriguez, Anal. Chem., 2016, 88, 4706–4713.
236 M. Asghari-Khiaei, B. R. Wood, P. Hojati-Talemi, A. Downes, D. McNaughtona and A. Mechlera, J. Raman Spectrosc., 2012, 43, 173–180.
237 W. Su and D. Roy, J. Vac. Sci. Technol., B: Nanotechnol. Microelectron.: Mater., Process., Meas., Phenom., 2013, 31, 041808.
238 N. Kumar, B. Stephanidis, R. Zenobi, A. J. Wain and D. Roy, Nanoscale, 2015, 7, 7133–7137.
239 R. Zhang, Y. Zhang, Z. C. Dong, S. Jiang, C. Zhang and L. G. Chen, Nature, 2013, 498, 82–86.
240 N. Kumar, S. Mignuzzi, W. Su and D. Roy, EPJ Tech. Instrum., 2015, 2, 9.
241 B. R. Wood, E. Baito, M. A. Khiaei, L. Tilley, S. Deed and T. Deckert-Gaudig, Nano Lett., 2011, 11, 1868–1873.
242 R. Bohme, M. Richter, D. Cialla, P. Rosch, V. Deckert and J. Popp, J. Raman Spectrosc., 2009, 40, 1452–1457.
243 T. Deckert-Gaudig, E. Baito and V. Deckert, Phys. Chem. Chem. Phys., 2009, 11, 7360–7362.
244 L. M. Malard, M. A. Pimenta, G. Dresselhaus and M. S. Dresselhaus, Phys. Rep., 2009, 473, 51–87.
245 E. M. v. Lantman, T. Deckert-Gaudig, A. J. G. Mank, V. Deckert and B. M. Weckhuysen, Nat. Nanotechnol., 2012, 7, 583–586.
246 C. E. Harvey and B. M. Weckhuysen, Catal. Lett., 2015, 145, 40–57.
247 H. Hartman, C. S. Wondergem, N. Kumar, A. v. d. Berg and B. M. Weckhuysen, J. Phys. Chem. Lett., 2016, 7, 1570–1584.
248 N. Jiang, D. Kuroski, E. A. Pozzi, N. Chiang, M. C. Hersam and R. P. V. Duyne, Chem. Phys. Lett., 2016, 659, 16–24.
249 T. Mino, Y. Saito and F. Verma, ACS Nano, 2014, 8, 10187–10195.
250 L. T. Nieman, G. M. Krampert and R. E. Martinez, Rev. Sci. Instrum., 2001, 72, 1691–1699.
A. Zuber, M. Purdey, E. Schartner, C. Forbes, B. van der Hoek, D. Giles, A. Abell, T. Monro and H. Ebendorff-Heidepriem, Sens. Actuators, B, 2016, 227, 117–127.

V. Singh, Z. Li, X. Zhou, X. Xu, J. Xu, A. Nand, H. Wen, H. Li, J. Zhu and J. Zhang, RSC Adv., 2016, 6, 3213–3218.

L. L. Yin, S. P. Wang, X. N. Shan, S. T. Zhang and N. J. Tao, Rev. Sci. Instrum., 2015, 86, 114101.

E. Kretschmann, Opt. Commun., 1972, 6, 185–187.

K. M. Shakesheff, X. Chen, M. C. Davies, A. Domb, C. J. Roberts, S. J. B. Tendler and P. M. Williams, Langmuir, 1995, 11, 3921–3927.

X. Chen, K. M. Shakesheff, M. C. Davies, J. Heller, C. J. Roberts, J. B. Tendler and P. M. Williams, J. Phys. Chem. B, 1999, 103, 11537–11542.

A. Baba, W. Knoll and R. Advincula, Rev. Sci. Instrum., 2006, 77, 064101.

L. Joergensen, B. Klösgen, A. C. Simonsen, J. Borch and E. Hagesæther, Int. J. Pharm., 2011, 411, 162–168.

K. Hall, T-H. Lee, A. I. Mechler, M. J. Swann and M.-I. Aguilar, Sci. Rep., 2014, 4, 5479.

X. Chen, M. C. Davies, C. J. Roberts, K. M. Shakesheff, S. J. B. Tendler, P. M. Williams and J. Davies, J. Vac. Sci. Technol., B: Microelectron. Nanometer Struct.-Process., Meas., Phenom., 1996, 14, 1582–1586.

S. Kitamura and M. Iwatsuki, Appl. Phys. Lett., 1998, 72, 3154.

M. Nonnenmacher, M. P. Oboyle and H. K. Wickramasinghe, Appl. Phys. Lett., 1991, 58, 2921.

D. Kohl, P. Mesquida and G. Schitter, Microelectron. Eng., 2017, 176, 28–32.

H. M. I. Jaim, R. A. Isaacs, S. N. Rashkeev, M. Kuklija, D. P. Cole, M. C. LeMieux, I. Jasiuk, S. Nilufar and L. G. Salamanca-Riba, Carbon, 2016, 107, 56–66.

S. Gunther, B. Kaulich, L. Gregoratti and M. Kiskinova, Prog. Surf. Sci., 2002, 70, 187–260.

H. Luth, Solid Surfaces, Interfaces and Thin Films, Springer, Berlin, 2001.

J. C. Gonzalez, K. L. Bunker and P. E. Russell, Appl. Phys. Lett., 2001, 79, 1567.

T. Glatzel, S. Sadewasser and M. C. Lux-Steiner, Appl. Surf. Sci., 2003, 210, 84–89.

U. Zerweck, C. Loppacher, T. Otto, S. Grafström and L. M. Eng, Phys. Rev. B: Condens. Matter Mater. Phys., 2005, 71, 125424.

Z. Ma, L. Kou, Y. Naitoh, Y. J. Li and Y. Sugawara, Nanotechnology, 2013, 24, 225701.

L. Polak, S. d. Man and R. J. Wijngaarden, Rev. Sci. Instrum., 2014, 85, 046111.

S. Barbet, M. Popoff, H. Diesinger, D. Deresmes, D. Théron and T. Mélion, J. Appl. Phys., 2014, 115, 144313.

J. Murawski, T. Graupner, P. Milde, R. Raupach, U. Zerweck-Trogisch and L. M. Eng, J. Appl. Phys., 2015, 118, 154302.

L. Collins, A. Belianinov, S. Somnath, N. Balke, S. V. Kalinin and S. Jesse, Sci. Rep., 2016, 6, 30557.

R. Borgani, D. Forchheimer, J. Bergqvist, R. A. Thorén, O. Ingañás and D. B. Haviland, Appl. Phys. Lett., 2014, 105, 143113.

Y. Sugawara, L. Kou, Z. Ma, T. Kamijo, Y. Naitoh and L. Y. Jun, Appl. Phys. Lett., 2012, 100, 223104.
399 M. Timofeeva, A. Bolshakov, P. D. Tovee, D. A. Zeze, V. G. Dubrovskii and O. V. Kolosov, *Ultramicroscopy*, 2016, 162, 42–51.

400 F. Menges, P. Mensch, H. Schmid, H. Riel, A. Stemmer and B. Gotsmann, *Nat. Commun.*, 2016, 7, 10874.

401 L. D. P. Lopez, S. Grauby, S. Dilhaire, M. Amine Salhi, W. Claeyts, S. Lefèvre and S. Volz, *Microelectron. J.*, 2004, 35, 797–803.

402 G. Hwang and O. Kwon, *Int. J. Therm. Sci.*, 2016, 108, 81–88.

403 S. Gomes, P. O. Chapuis, F. Nepveu, N. Trannoy, S. Volz, B. Charlot, G. Tessier, S. Dilhaire, B. Cretin and P. Vairac, *IEEE Trans. Compon. Packag. Technol.*, 2007, 30, 424–431.

404 G. B. M. Fiege, F. J. Niedernostheide, H. J. Schulze, R. Barthelmeß and L. J. Balk, *Microelectron. Reliab.*, 1999, 39, 1149–1152.

405 M. Tortello, S. Colonna, M. Bernal, J. Gomez, M. Pavese, C. Novara, F. Giorgis, M. Maggio, G. Guerra, G. Saracco, R. S. Gonnelli and A. Fina, *Carbon*, 2016, 109, 390–401.

406 L. Shi, J. Zhou, P. Kim, A. Bachtold, A. Majumdar and P. L. McEuen, *J. Appl. Phys.*, 2009, 105, 104306.

407 Y.-J. Yu, M. Y. Han, S. Berciaud, A. B. Georgescu, T. F. Heinz, L. E. Brus, K. S. Kim and P. Kim, *Appl. Phys. Lett.*, 2011, 99, 183105.

408 F. Menges, H. Riel, A. Stemmer and B. Gotsmann, *Nano Lett.*, 2012, 12, 596–601.

409 S. S. Kharintsev, E. A. Chernykh, A. I. Fishman, S. K. Saikin, A. M. Alekseev and M. K. Salakhov, *J. Phys. Chem. C*, 2017, 121, 3007–3012.

410 S. Volz, X. Feng, C. Fuentes, P. Guérin and M. Jaouen, *Int. J. Thermophys.*, 2002, 23, 1645–1657.

411 Y. Zhang, E. E. Castillo, R. J. Mehta, G. Ramanath and T. Borca-Tasciuc, *Rev. Sci. Instrum.*, 2011, 82, 024902.

412 T. Borca-Tasciuc, *Annu. Rev. Heat Transfer*, 2013, 16, 211–258.

413 P. J. Newby, B. Canut, J.-M. Bluet, S. Gomès, M. Isaiev, R. Burbelo, K. Termenzidis, P. Chantrenne, L. G. Fréchette and V. Lysenko, *J. Appl. Phys.*, 2013, 114, 014903.

414 S. Gomès, L. David, V. Lysenko, A. Descamps, T. Nychyporuk and M. Raynaud, *J. Phys. D: Appl. Phys.*, 2007, 40, 6677.

415 M. Luna, J. Colchero and A. M. Baró, *J. Phys. Chem. B*, 1999, 103, 9576–9581.

416 M. Chirtoc, J. Gibkes, R. Wernhardt, J. Pelzl and A. Wieck, *Rev. Sci. Instrum.*, 2008, 79, 8.