Potential Reproducibility of Potassium-Selective Electrodes Having Perfluorinated Alkanoate Side Chain Functionalized Poly(3,4-ethylenedioxythiophene) as a Hydrophobic Solid Contact

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ABSTRACT: The irreproducibility of the standard potential (E°) is probably the last major challenge for the commercialization of solid-contact ion-selective electrodes (SCISEs) as single-use or wearable sensors. To overcome this issue, we are introducing for the first time a perfluorinated alkanoate side chain functionalized poly(3,4-ethylenedioxythiophene) (PEDOTF) as a hydrophobic SC in potassium-selective electrodes (K-SCISEs) based on plasticized poly(vinyl chloride). The SC incorporates the tetrakis(pentafluorophenyl)borate (TFAB⁻) anion, which is also present as a lipophilic additive in the ion-selective membrane (ISM), thus ensuring thermodynamic reversibility at the SC/ISM interface and improving the potential reproducibility of the electrodes. We show here that the PEDOTF-TFAB solid contact, which was prepolared prior to the ISM deposition to either its half or fully conducting form (i.e., different oxidation states) in acetonitrile containing 0.01 M KTFAB, had a very stable open-circuit potential and an outstanding potential reproducibility of only ±0.5 mV (n = 6) for 1 h in the same solution after the prepolarization. This shows that the oxidation state of the highly hydrophobic PEDOTF-TFAB film (water contact angle 133°) is stable over time and can be precisely controlled with prepolarization. The SC was also not light sensitive, which is normally a disadvantage of conducting polymer SCs. After the ISM deposition, the standard deviation of the E° of the K-SCISEs prepared on glassy carbon was ±3.0 mV (n = 5), which is the same as that for conventional liquid contact K-ISEs. This indicates that the ISM deposition is the main source for the potential irreproducibility of the K-SCISEs, which has been overlooked previously.

Solid-contact ion-selective electrodes (SCISEs) have been the subject of intensive research. Clearly, the replacement of the aqueous liquid contact in conventional ISEs with a solid material is appealing not only in terms of widening their applicability by withstanding higher pressures (deep water measurements) or temperatures but also in terms of easier mass production and robust miniaturization. The most popular ion-to-electron transducers, i.e., solid contacts (SC), have been until now electrically conducting polymers (ECP), different carbon materials with large capacitance, and redox compounds. Recently various new SCs have also gained popularity, such as tetraathiafulvalene (TTF) and 7,7,8,8-tetracyanoquinodimethane (TCNQ) and their radical salts, intercalation compounds (LiFePO4/FePO4), Prussian blue analogues, KBr/AgBr, fullerences, submicron porous carbon spheres, gold nanoparticles, molybdenum disulfide, and metal–organic frameworks (MOF), and different types of composite materials.

Initially the main aim of the research in this field was to develop robust and miniaturized SCISEs that match the excellent potential stability of the conventional ISEs with a potential drift of less than ca. 0.1 mV h⁻¹. However, with the increasing interest in single-use and wearable sensors, the efforts became largely oriented toward the development of SCISEs for calibration-free measurements. ISEs seem ideal devices in this respect, as they follow the Nernst equation: i.e., the slope of the linear part of the calibration curve (E vs log a) is constant for a given analyte ion charge and temperature. Properly designed SCISEs have slopes very close to the ideal Nernstian slope, but their standard potentials (E°) determined...
at $a = 0$ usually show an unacceptable large variation. Not only are the $E^\circ$ values difficult to predict theoretically but also even the very same preparation method may lead to unrepeatable values, which is currently the biggest challenge hampering commercialization of the SCISEs.

Although some very good $E^\circ$ reproducibilities have been reported, it is still problematic to objectively compare these values due to the lack of a standardized test protocol for the $E^\circ$ determination. The SCISEs may have been exposed to different long periods before the standard deviation (SD) of $E^\circ$ was determined. While a divergence in time of the $E^\circ$ values is the most common, there are also examples of the opposite. For example, $K^+$-selective divergence in time of the values due to the lack of a standardized test protocol for the reported, it is still problematic to objectively compare these conditioning or measurements for di determination. The SCISEs may have been exposed to the standard deviation (SD) of commercialization of the SCISEs.

$\pm$\textsuperscript{0.7 mV ($n = 4$) and a very low potential drift of only 69 $\mu$V h$^{-1}$ during the test period of 46 days, after which they still had a good $E^\circ$ reproducibility of $\pm$3.1 mV. Other studies, including that of Guzinski et al. using PEDOT-C$_x$, as the SC, seem to conclusively support the need for highly hydrophobic SCs as one of the main prerequisites for obtaining stable and reproducible electrode potentials. Despite the good $E^\circ$ reproducibility of the K-SCISEs based on PPy-PFOS, we observed in interlaboratory studies that it was challenging to get a very good $E^\circ$ reproducibility with a larger number of SCISEs.

We have therefore conducted a systematic study to understand the reasons for the $E^\circ$ irreproducibility of K-SCISEs having poly(3,4-ethylenedioxythiophene) (PEDOT) as the SC. For the first time a highly hydrophobic perfluorinated alkanoate side chain functionalized PEDOT$^{44,45}$ (PEDOTF) has been applied as the SC. It incorporates the tetrakis(pentafluorophenyl)borate anion (TFAB$^-$) in its structure to enhance the hydrophobicity of the conducting form of the ECP-SC. To further optimize the SCISE design, we have also added TFAB$^-$ to the ISM as a lipophilic cation exchanger, which we expect will result in a well-defined and reproducible phase boundary potential at the SC/ISM interface. The results presented in this work show that the deposition of the PVC-ISM on the SC is the main source causing the potential irreproducibility of the K-SCISEs, which has been overlooked previously.

### EXPERIMENTAL SECTION

**Chemicals.** As described in the Supporting Information, fluorinated 3,4-ethylenedioxythiophene with a perfluorooctyl side chain (EDOTF) was custom-synthesized from hydroxymethyl EDOT (95%) and perfluorooctane sulfonic acid (97%) obtained from Sigma-Aldrich. High-molecular-weight PV (HMW PVC), bis(2-ethylhexyl) sebacate (DOS), potassium ionophore I (valinomycin), and tetrahydrofuran (THF), all Selectophore grade, and anhydrous acetonitrile (ACN; 99.5%) were purchased from Sigma-Aldrich. KTFAB (97%; Figure S-1) was obtained from Alfa Aesar, and KCl (99.999%, Suprapur grade) was received from Merck Millipore. All aqueous solutions were prepared from deionized water (DIW) with a resistivity of 18.2 MΩ cm (ELGA).

**Electropolymerization of EDOTF and Prepolarization of the PEDOT-SCs.** The electropolymerization (EP) of EDOTF was done galvanostatically at 0.5 mA cm$^{-2}$ to 0.5 C cm$^{-2}$ (controlled by a Autolab PGSTAT potentiostat) in freshly made ACN solutions of 0.01 M EDOTF and 0.01 M KTFAB. A three-electrode setup was used, where a glassy-carbon (GC) or gold electrode ($d = 1.6$ mm; incorporated in a polyester ether ketone (PEEK) body with an outer diameter of 6.0 mm; Bio-Logic Science Instruments), a Pt wire, and an Ag wire served as working (WE), counter, and pseudo-reference, respectively. The WE was polished prior to the EP with a 0.05 μm alumina suspension, rinsed thoroughly with ethanol.
and DIW followed by ultrasonication for 5 min in DIW, and finally rinsed again with ethanol and DIW. The electropolymerization solution was first purged with \( N_2 \) for 15 min immediately before use and then blanketed during the polymerization. After the EP, the PEDOTF-TFAB films were rinsed with ACN and prepolared in deaerated 0.01 M KTFAB-ACN at either 0.22 or 0.40 V for 5 min using the same three-electrode setup as above. Finally, the PEDOTF-SCs were rinsed with either ACN or THF, as explained in the Results and Discussion, before they were allowed to dry for ca. 10 min and rinsed with either ACN or THF, as explained in the Results and Discussion, before they were allowed to dry for ca. 10 min in ambient air prior to the drop-casting of the PVC-ISM on top of the PEDOTF-SC. Some of the PEDOTF-TFAB films were also characterized after the EP with cyclic voltammetry (CV) in the potential range of \(-0.5 \) V to \(+0.7 \) V in deaerated 0.01 M KTFAB-ACN with scan rates \( (\nu) \) of 5, 10, and 20 mV s\(^{-1}\) using the same three-electrode setup as above. All electrode potentials in this work related to the electropolymrization of EDOTF, prepolariation, and characterizations of the PEDOTF-SCs refer to the Ag wire acting as a pseudoreference electrode.

**K**–Selective SCISE Fabrication. The ISM had the following composition: 32.9% (w/w) HMW PVC, 65.7% DOS, 1.06% valinomycin, and 0.34% KTFAB. The components were dissolved in 1 mL of THF to produce a solution with 20% dry weight. A 40 \( \mu \)L portion of the ISM cocktail solution was deposited by drop-casting onto the PEDOTF-SCs in two consecutive steps (2 x 20 \( \mu \)L), and the PVC-ISM with a thickness of ca. 220 \( \mu \)m were allowed to dry overnight in ambient air. We compared the initial potential stability and \( E^\circ \) reproducibility of the K-SCISE with those of their conventional liquid contact counterparts having the same ISM composition. The latter were prepared by pouring 1.5 mL of an ISM cocktail (10% w/w in THF) into a glass ring (\( d = 24.4 \) mm) fixed on a glass plate. The PVC-ISM was allowed to dry overnight before circular membranes with a diameter of 7 mm were punched (thickness ca. 200 \( \mu \)m) out of it and mounted into conventional Philips IS 561 electrode bodies (Möller Glasbläserei, Zürich, Switzerland) with 0.01 M KCl as the inner filling solution.

**Potentiometric Measurements.** We used a 16-channel high input impedance voltmeter (10\(^9\) \( \Omega \), Lawson Laboratories, Malvern, PA, USA) in all potentiometric measurements. The potential stability of the PEDOTF-SCs was determined in 0.01 M KTFAB-ACN for 1 h, whereas the initial potential stabilities of the K-SCISEs were measured in 0.01 M KCl for 24 h. The K-SCISEs were calibrated from 10\(^{-1}\) to 10\(^{-9}\) M KCl, and the potential readings at every concentration were taken after 5 min in quiescent solutions. In all aqueous solutions, we used a double-junction Ag/AgCl/3 M KCl//1 M LiOAc as the RE (No. 6.0729.100, Metrohm AG). The potentiometric aqueous layer test was done with fully conditioned SCISEs by changing the solution from 0.1 M KCl to 0.1 M NaCl (24 h) and then back to 0.1 M KCl (24 h). The light sensitivity of the PEDOTF-SC (without ISM) was measured in 0.01 M KTFAB-ACN by keeping the electrodes first in room light (10 min) and then exposing them to complete darkness (10 min) and finally to intense cold light (10 min, >1.6 x 10\(^4\) lx; Leica CLS 150XE light source\(^{41}\)).

**Water Contact Angles and SEM Measurements.** Water droplets were placed on PEDOTF-TFAB films (\( d = 5.0 \) mm) that had been prepolarized to \(-0.50, 0.20, \) and 0.50 V. We recorded images of the water droplets with a Dyno-Lite USB digital microscope and determined the WCAs from the images with the Inkscape 0.92.3 software. We measured the surface morphology and the film thickness of the PEDOTF-SC prepared on a Pt-sputtered ZnSe reflection element (see below) with the LEO1530 Gemini FEGSEM instrument.

**Water Uptake of the PEDOTF-SC.** We measured the diffusion of water in the ca. 1.8 \( \mu \)m thick PEDOTF-SC with the FTIR-ATR technique for 24 h in 0.01 M KCl. The film was deposited by electropolymerization on the Pt-sputtered ZnSe reflection element. Prior to the water uptake measurements, we prepolarized the SC to its fully conducting form (positively charged) at 0.40 V for 5 min to maximize its water uptake. The experimental details of the water uptake measurements are given in the Supporting Information. The experimental setup and the modeling of the water diffusion coefficients have been thoroughly described in detail elsewhere.\(^{9,46}\)

### RESULTS AND DISCUSSION

We report here for the first time the electropolymrization of EDOTF with the TFAB\(^{+} \) anion as the charge-compensating counterion on GC and gold (Au) substrates. Figure S-2 shows the CVs recorded during the electropolymrization of 0.01 M EDOTF in 0.01 M KTFAB-ACN on GC in the potential range of \(-0.9 \) to \(+1.5 \) V. They reveal that the polymerization of EDOTF starts at ca. 1.3 V, and the increasing anodic and cathodic currents confirm that the film grows in thickness during each potential cycle. However, we found that the PEDOTF film growth was not fully reproducible with CV and the PEDOTF-SC film thickness could not therefore be controlled precisely. Some GC electrodes required a higher anodic end potential for the film formation, which may be due to slightly different surface properties of the commercial GC-PEEK electrodes used in this study. This assumption is supported by comparing the anodic and cathodic peak potentials (\( E_{pa} \) and \( E_{pc} \)) given by the electrode manufacturer for the 12 GC-PEEK electrodes that were used in this study. The manufacturer had measured the \( E_{pa} \) and \( E_{pc} \) after the electrode fabrication in 1 mM K\(_4\)Fe(CN)\(_6\) with 1.0 M KNO\(_3\) as the background electrolyte. The comparison shows that the \( E_{pa} \) varied between 237 and 295 mV for the 12 GC-PEEK electrodes that were supposed to be identical (electrodes 1–9, 289 ± 4 mV; electrodes 10–12, 238 ± 1 mV). The corresponding \( E_{pc} \) values were 162–225 mV (electrodes 1–9, 220 ± 6 mV; electrodes 10–12, 163 ± 1 mV), and the peak separation (\( \Delta E_{p} = E_{pa} - E_{pc} \)) was 64–75 mV. It is known that the electron transfer for GC is a second-order reaction, which is influenced if the electrodes are polished or modified with GC-PEEK layers, which may be due to the different surface properties of the commercial GC-PEEK electrodes used in this study. Figure S-3 shows the \( E_{pa} \) and \( E_{pc} \) after the electrode fabrication in 1 mM K\(_4\)Fe(CN)\(_6\) with 1.0 M KNO\(_3\) as the background electrolyte. The comparison shows that the \( E_{pa} \) varied between 237 and 295 mV for the 12 GC-PEEK electrodes that were supposed to be identical (electrodes 1–9, 289 ± 4 mV; electrodes 10–12, 238 ± 1 mV). The corresponding \( E_{pc} \) values were 162–225 mV (electrodes 1–9, 220 ± 6 mV; electrodes 10–12, 163 ± 1 mV), and the peak separation (\( \Delta E_{p} = E_{pa} - E_{pc} \)) was 64–75 mV. It is known that the electron transfer for GC is a second-order reaction, which is influenced if the electrodes are polished or modified with GC-PEEK layers, which may be due to the different surface properties of the commercial GC-PEEK electrodes used in this study.
electrodes were typically 292–294 and 215–217 mV, respectively. To further improve the reproducibility of the electropolymerization, the PEDOT-TFAB electrodes were individually electropolymerized from fresh monomer solutions ($V = 3 \text{ mL}$, Figure S-4). The formed PEDOTF-SCs were characterized by CV in 0.01 M KTFAB-ACN in the potential range of $-0.5$ to $+0.5$ V (Figure 1). The CVs show that the PEDOTF film converts to the electrically conducting form at $E > -0.20 \text{ V}$. At $v = 5 \text{ mV s}^{-1}$, the $E_p$ and $E_{pc}$ values were 0.32 and 0.13 V, respectively, but shifted to 0.42 and 0.02 V for $v = 20 \text{ mV s}^{-1}$, indicating that the electrode transfer becomes slightly more sluggish at higher scan rates.

SEM images (Figure S-5) revealed that the PEDOT-TFAB film has a uniform surface morphology and a relatively open surface structure with sharper polymer bundles pointing out from the surface, which are expected to further lower the wettability of the hydrophobic polymer film. To confirm this, we performed WCA measurements on PEDOTF-SCs prepolarized to $-0.5 \text{ V}$ (nonconducting form), 0.20 V (half conducting form), and 0.5 V (fully conducting form) in 0.01 M KTFAB-ACN. In agreement with our expectations, the WCA of PEDOTF was ca. 131–133° irrespective of its conducting state (insets in Figure 1), proving that both the half and fully conducting forms are highly hydrophobic, which is crucial for preventing the detrimental aqueous layer formation beneath the ISM causing potential instability of the SCISEs. The WCAs reported here are slightly lower than those measured by Luo et al. for a PEDOTF film prepared with a constant potential of 1.4 V at 0 °C (131.9–150.5°) but are in very good accordance with the WCA of PEDOT-C$_{14}$ (136 ± 5°) and higher than those for polyazulene doped with PF$_6^{-}$ (PAz-PF$_6$; 126 ± 14°) chemically prepared polyoctylthiophene (POT; ca. 110°),$^{35,42}$ and PPy-PFOS (97 ± 5°).$^{10}

The high hydrophobicity of the PEDOTF-SC film was confirmed by measuring the water diffusion through the film with the FTIR-ATR technique$^{46,50-52}$ when it was placed in contact with 0.01 M KCl solution (Figure 2). In evaluating the FTIR spectra, it must be kept in mind that this technique is very sensitive and is able to detect traces of water, in contrast to the potentiometric aqueous layer test.$^{54,55}$ The spectra in the wavenumber region of ca. 3000–3700 cm$^{-1}$ (OH stretching) reveal that minor amounts of water have diffused through the PEDOTF-SC to the vicinity of the SC/ZnSe interface already after 5 min when the SC is fully exposed to water. The amount of water increases very slowly during the whole measurement until a saturation level is reached after ca. 20 h. It is expected that some water diffusion will always take place in all types of (slightly) porous SCs, showing the challenge in completely blocking the water diffusion. Mathematical modeling of the water uptake showed that it can be described with three diffusion coefficients, $D_1 = 6.6 \times 10^{-11} \text{ cm}^2 \text{s}^{-1}$, $D_2 = 1.9 \times 10^{-12} \text{ cm}^2 \text{s}^{-1}$, and $D_3 = 2.8 \times 10^{-13} \text{ cm}^2 \text{s}^{-1}$, indicating that the water diffusion in the PEDOTF-SC is slightly higher than in the PPy-PFOS solid contact$^{2}$ but lower than in the POT-SC.$^{51}$ However, as the surface of most conducting polymers is relatively uneven, it is difficult to determine the film thickness with the highest precision, adding some uncertainty to the reported water diffusion coefficients.

The SC should preferably have a relatively high capacitance to provide the SCISEs with a stable potential.$^{4}$ Electrochemical impedance measurements showed that the redox capacitance of the PEDOTF-SC was ca. 40 mF cm$^{-2}$ (Figure S-6). This is sufficiently high for the PEDOTF-SC to act as very efficient redox buffer and ion-to-electron transducer in the K-SCISEs. The capacitance is considerably higher than for PEDOT prepared with polystyrenesulfonate (15 mF cm$^{-2}$),$^{54,55}$ similar to that for PAz-PF$_6$ (45 mF cm$^{-2}$),$^{42}$ and much lower than that for a composite consisting of polyaniline and reduced graphene oxide (77 mF cm$^{-2}$).$^{55}$ All transducers were prepared with the same charge as for the PEDOTF-SC.

The lipophilic TFAB$^{-}$ anion is present both in the PVC-ISM and in the PEDOTF-SC to ensure thermodynamic reversibility at the SC/ISM interface. We measured therefore the potentiometric response of the SC in 10$^{-4}$–10$^{-2}$ M KTFAB-ACN and in aqueous 10$^{-4}$–10$^{-1}$ M KCl solutions to determine if the PEDOTF-SC exchange anions or cations. We found that the SC had a super-Nernstian anionic response in KTFAB-ACN solutions, revealing that it is exchanging TFAB$^{-}$ anions when the SC is in contact with an organic phase: i.e., the PVC-ISM. In KCl solutions, we observed a sub-Nernstian K$^+$ response indicating that the highly hydrophobic TFAB$^{-}$ anion cannot leave the SC and enter the aqueous phase. We can therefore conclude that the PEDOTF-SC exchanges TFAB$^{-}$ anions when it functions as an ion-to-electron transducer beneath the K$^+$-selective PVC-ISM, which
we expect will improve the potential reproducibility of the electrodes. However, we can speculate that a certain degree of K⁺ exchange may also occur in the presence of small amounts of water at the SC/ISM interface.

The light sensitivity can be a drawback for most ECPs, especially POT, although many ECPs that we have used as SCs in SCISEs, such as PPY-PFOS and PAz-PF₆ are completely light insensitive beneath the ISM. We therefore exposed the PEDOTF-SC in 0.01 M KTFAB-ACN (to exclude the potential of water at the SC/ISM interface. We let the SCs dry in ambient air for ca. 10 min and a potential reproducibility (given as SD) of ±0.5 mV (n = 6) measured in 0.01 M KTFAB-ACN for 1 h after polarization in the same solution to 0.22 V (vs a Ag wire) for 5 min. The minor potential drift is due to the evaporation of ACN from the solution.

sensitivity of the bare PEDOTF-SC, thus making it a most suitable SC material for SCISEs. The light sensitivity test was restricted to 30 min due to the high volatility of ACN, which is the reason for the slow potential drift observed in Figure 3.

To identify what causes the $E^\circ$ irreproducibility of the K-SCISEs, we started by measuring the potential stability of the bare PEDOTF-SC before the ISM was deposited on top of it by drop-casting. The PEDOTF-SC was first prepolarized to 0.22 V for 5 min in 0.01 M KTFAB-ACN, and after that, its open-circuit potential stability and reproducibility were measured in the same electrolyte solution for 1 h (Figure 4).

The PEDOTF-SCs showed an outstanding potential stability and a potential reproducibility (given as the SD) of ±0.5 mV (n = 6) during the whole test period. This shows that it is possible to adjust the conducting state of the PEDOTF-SC to a desired level that is very stable over time. The measurement proved also that differences in the initial surface conditions of the GC substrates do not influence the potential reproducibility of the prepolarized SCs, and we can therefore exclude that they cause the $E^\circ$ irreproducibility of the SCISEs.

Since the PEDOTF-SC will be in contact with THF during the drop-casting of the PVC-ISM on top of it, we studied also how the potential reproducibility was influenced by keeping the SC in contact with a pure stirred THF solution for different long times up to 30 min. After the SC was kept in pure THF solution for 0.25, 0.5, 1, 2, 5, 10, 15, or 30 min, its potential reproducibility was determined at the open-circuit potential in 0.01 M KTFAB-ACN (Figure 5).

We compared the potential reproducibilities obtained after the THF treatment with a PEDOTF-SC that had been exposed to pure ACN in an identical measuring sequence. This was done because the SC is rinsed with pure ACN after the prepolarization in 0.01 M KTFAB-ACN and it can possibly influence its doping level (i.e. oxidation state) due to leaching of TFAB⁻ anions into the organic solvent. Figure 5 shows that the contact time with THF does not influence the potential reproducibility to any significant extent, especially for t ≤ 5 min (SD < 1.0 mV). Even for greater exposure times there is no clearly observed trend, and since the potential reproducibility is still ±0.6 mV after the contact time of 30 min with THF, which is the same as for t = 0.25 min, it is unlikely that THF will affect the potential of the PEDOTF-SC during the drop-casting and overnight drying of the PVC-ISM. However, we found that a contact time longer than 5 min with ACN had a negative effect on the potential reproducibility. Hence, the PEDOTF-SC should be rinsed only briefly to remove residues of the KTFAB electrolyte salt from its surface. In another experiment described in Figure S-7, we show that is essential to rinse the SC with ACN after the prepolarization to avoid severe deterioration of the detection limit (LOD) and selectivity coefficients of the K-SCISEs.

We fabricated the K-SCISEs on GC and Au substrates to study how the substrate material influences the initial potential stability and reproducibility of the electrodes (Figure 6 and Figure S-8). The PEDOTF-SCs were prepolarized either to the half-conducting form (0.22 V) or fully conducting form (0.40 V) in 0.01 M KTFAB-ACN. They were then kept in a stirred ACN solution for 30 s to wash off KTFAB residues from the SC surface. We let the SCs dry in ambient air for ca. 10 min prior to the deposition of the PVC-ISM by drop-casting.
When the SCISEs were in contact with 0.01 M KCl solution for the first time, the potential of the K-SCISEs prepared on GC substrates stabilized quickly within ca. 3–5 min independent of the prepolarization potential of the PEDOTF-SC (Figure 6), which is only slightly longer than that for the conventional liquid contact K-ISEs (ca. 2 min). We obtained the same stabilization time of 3–5 min for the SCISEs prepared on Au substrates with the PEDOTF-SC prepolarized to 0.22 V, while the electrodes prepolarized to 0.40 V had a considerably longer stabilization time of ca. 20 min (Figure S-8).

In Table 1, we have summarized the potential drifts and potential reproducibilities (SD) of the K-SCISEs and conventional liquid contact K-ISEs measured during the initial potential stability measurement. The SCISEs prepared on the GC substrates had a slightly better potential reproducibility, especially after 24 h in contact with 0.01 KCl, than the SCISEs having Au as the substrate material. Among all electrodes, the K-SCISEs prepared on GC and prepolarized at 0.40 V had the best potential reproducibility of only ±2.3 mV at the beginning of the test (t = 0 h) and ±2.7 mV after 24 h. This is practically the same as for the conventional K-ISEs, which showed ±2.1 and ±2.9 mV at the beginning of the test and after 24 h, respectively. This indicates that the prepolarized K-SCISEs have response characteristics that are equal to those of the conventional K-ISEs. It also shows that the prepolarization of the SC is essential to obtain electrodes with high $E^o$ reproducibility. We demonstrate this in Figure S-9 for K-SCISEs having nonpolarized PEDOTF-SCs. The potential response of one of the SCISEs deviates considerably (>300 mV) from the other five electrodes, which show a relatively good $E^o$ reproducibility of ±5.2 mV in the beginning of the initial potential stability test (Table 1), but ±10.7 mV already after 24 h in 0.01 M KCl.

We observed that the K-SCISEs that were prepolarized to the half conducting form (0.22 V) had a lower initial potential drift in comparison to the electrodes prepolarized to the fully conducting form (0.40 V). The K-SCISEs fabricated on GC and prepolarized to 0.22 V had the lowest potential drift of only $-56 \pm 24 \mu V h^{-1}$ during the first 24 h in 0.01 M KCl, which is comparable to the drift of the conventional K-ISEs (32 ± 47 $\mu V h^{-1}$). The reasons for the higher drift obtained for the K-SCISEs prepolarized at 0.40 V is still unclear. However, we speculate that the long-term stability of the fully oxidized form of PEDOTF-SC is lower than that for the half oxidized form (0.22 V), which has approximately equal concentrations of conducting and nonconducting polymer segments, thus providing the SCs with a better redox buffer capacity: e.g., against the influence of oxygen. Figure S-10 shows that the potential of the K-SCISE prepared on GC and prepolarized at 0.22 V was insensitive to O2 and CO2, while these gases were purged through 0.1 M KCl for 95 and 60 min, respectively. We note also that we did not study further the potential response characteristics of the K-SCISEs fabricated on the Au substrates due to their slightly worse potential reproducibility in comparison to GC.

Completely new Au and GC electrodes were also bought for this purpose and were compared to older GC electrodes that were purchased in 2010, which had been in extensive use earlier. We could not find any noticeable differences in the initial potential stability and reproducibility between these GC electrodes and the new GC electrodes that were purchased for this project.

In Figure 7, the calibration curves show that the K-SCISEs prepared on GC with the PEDOTF-SC prepolarized to the fully conducting form had in practice the same potentiometric response as the conventional K-ISEs. The $E^o$ reproducibility (SD), slope, and LOD of the K-SCISEs and the conventional liquid contact K-ISE for comparison.

### Table 1. Initial Potential Drift and Reproducibility in 0.01 M KCl, the Potentiometric Slope, and the Standard Deviation (SD) of the Standard Potential ($E^o$) of the K-SCISEs

| $E_{prep}$ (V) | substrate | $n$ | potential drift ($\mu V h^{-1}$) | $E^o$ (SD, mV) |
|----------------|-----------|-----|-------------------------------|---------------|
| none | GC | 5 | -1100 ± 200 | 5.2 | 10.7 | 58.2 ± 0.7 | 10.9 |
| 0.22 | GC | 5 | -56 ± 24 | 7.5 | 5.9 | 59.5 ± 0.2 | 5.9 |
| 0.4 | GC | 5 | 950 ± 130 | 3.3 | 2.7 | 58.1 ± 0.6 | 3.0 |
| conventional K-ISE | Au | 4 | 32 ± 47 | 2.1 | 2.9 | 57.8 ± 0.5 | 3.0 |
| 0.22 | Au | 4 | 130 ± 210 | 4.0 | 6.4 | N/A | N/A |
| 0.4 | Au | 4 | -660 ± 330 | 7.1 | 7.8 | N/A | N/A |

*We show the conventional liquid contact K-ISE for comparison. *Prepolarization potential of the PEDOTF-SC vs a Ag wire in 0.01 M KTFAB-ACN. *Number of electrodes. *Determined between $t = 0.15$ and 24 h. *Determined between $t = 0.10$ and 24 h. *Determined in the concentration range of $10^{-5}-10^{-1}$ M KCl. $s_n = 4$. *Not measured due to the worse potential reproducibility in comparison to that for the K-SCISEs prepared on GC substrates.
The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acs.analchem.9b01587.

EDOTF synthesis, GC substrates (CV characterization), PEDOTF-SC (SEM images, water uptake (experimental description), electropolymerization (CV, constant potential), impedance spectra) SCISEs (O2 and CO2 sensitivity (experimental description), initial potential stability, and reproducibility (Au substrates), calibration graphs, chronopotentiograms, impedance spectra, and selectivity coefficients) (PDF)

Author Contributions
M.B. synthesized EDOTF. S.P. carried out the experimental work except for Figure 1 and Figures S-2 and S-6. T.L. planned the work with S.P. and R.E.G. and wrote the first manuscript.

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