Advanced Gastric Cancer and Perfusion Imaging Using a Multidetector Row Computed Tomography: Correlation with Prognostic Determinants

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Objective: To investigate the relationship between the perfusion CT features and the clinicopathologically determined prognostic factors in advanced gastric cancer cases.

Materials and Methods: A perfusion CT was performed on 31 patients with gastric cancer one week before surgery using a 16-channel multi-detector CT (MDCT) instrument. The data were analyzed with commercially available software to calculate tumor blood flow (BF), blood volume (BV), mean transit time (MTT), and permeability surface (PS). The microvessel density (MVD), was evaluated by immunohistochemical staining of the surgical specimens with anti-CD34. All of the findings were analyzed prospectively and correlated with the clinicopathological findings, which included histological grading, presence of lymph node metastasis, serosal involvement, distant metastasis, tumor, node, metastasis (TNM) staging, and MVD. The statistical analyses used included the Student’s t-test and the Spearman rank correlation were performed in SPSS 11.5.

Results: The mean perfusion values and MVD for tumors were as follows: BF (48.14 ± 16.46 ml/100 g/min), BV (6.70 ± 2.95 ml/100 g), MTT (11.75 ± 4.02 s), PS (14.17 ± 5.23 ml/100 g/min) and MVD (41.7 ± 11.53). Moreover, a significant difference in the PS values was found between patients with or without lymphatic involvement (p = 0.038), as well as with different histological grades (p = 0.04) and TNM stagings (p = 0.026). However, BF, BV, MTT, and MVD of gastric cancer revealed no significant relationship with the clinicopathological findings described above (p > 0.05).

Conclusion: The perfusion CT values of the permeable surface could serve as a useful prognostic indicator in patients with advanced gastric cancer.

With a mortality rate as high as 25 in 100,000, the prognosis of gastric cancer in China is very poor (1), and is closely related to TNM (tumor, node, metastasis) staging, histological classification and differentiation, lymphatic metastasis, as well as serosal infiltration (2, 3). Angiogenesis was originally reported by Folkman (4) in 1971, as the process of new blood vessel development, and reflects the generation of a new blood supply into tumor tissue that is now regarded as a prognostic indicator for several tumors. Generally, a tumor is measured by its microvessel density (MVD), which is a somewhat invasive technique, depending on the availability of postoperative tissue or adequate biopsy material (5).

Though multi-detector CT (MDCT) has been used for the staging of gastric carcinoma, the morphological features could not reflect the physiologic tissue parameters. Consequently, no adequate imaging modality has been reliable enough to predict the prognosis or to assist in the selection of the right patients for extended surgical...
procedures and for trials of adjuvant chemotherapy. The advent of spiral CT systems in the 1990s enabled perfusion scans to be performed with MDCT, thus broadening the technique’s availability, and permitting the measurement of the tumor vascular physiology in the brain, lung, liver, neck, and breast (6–8). The method could also be useful for assessing risk-stratification and therapeutic monitoring (9). Currently, the major clinical applications for perfusion CTs include acute stroke and oncology cases, such as tumor grading in cerebral glioma and lymphoma, and the prediction of tumor response to radiotherapy (6, 10). The relationship between the perfusion values and the prognosis of gastric cancer has, to the best of our knowledge, not been reported. The purpose of this study was to evaluate the relationship between perfusion CT and clinicopathological features of gastric adenocarcinoma and its potential as a novel prognostic predictor.

**MATERIALS AND METHODS**

**Patients**

Thirty one cases of pathologically proven gastric cancer occurring from March 2002 to March 2005 were prospectively included in this study. The patient records and the pertinent clinical data are shown in Table 1 and include tumor size (greatest diameter), pathological TNM (pTNM) staging (UICC 1997) and WHO histological grading (11) as described: well differentiated = an adenocarcinoma with well-developed glands and often resembling a metaplastic intestinal epithelium; moderately differentiated = an adenocarcinoma intermediate between the well differentiated and poorly differentiated; poorly differentiated = an adenocarcinoma composed of highly irregular glands that are recognized with difficulty, or single cells that remain isolated or are arranged in small to large clusters with mucin secretions or acinar structures.

A CT perfusion was approved by the Hospital Ethics Committee and a patient consent was obtained before imaging. All tumors were resected via a surgical procedure at one week after MDCT scanning (GE-Lightspeed, GE Medical Systems, Milwaukee, WI).

**Perfusion CT Technique**

Following a 1,000–1,200 ml oral dose of water, and a 20 mg intravenous injection of Scopolamine (Boehringer Ingelheim, Germany), a perfusion scan was performed in a 16-section MDCT cine period lasting 60 sec. The patients were instructed to practice a gentle breathing technique while scanning, and were fixed with an abdominal belt. The lesion was localized on the non-enhanced CT scan with a 2 cm tumor region of interest defined by an experienced radiologist. The dynamic scan was acquired at this level, performed at a static table position during an intravenous bolus of 50 ml in nonionic iodinated contrast

| Table 1. Clinical Characteristics of the Patients (n = 31) |
|----------------------------------|
| **Sex** | Male | 20 |
| | Female | 11 |
| **Age** | 42 - 79 yr (mean 62 yr) |
| **Size of tumor** | 3.3 - 8.4 cm (mean 4.2 cm) |
| **Depth of invasion** | pT2 | 10 |
| | pT3 | 15 |
| | pT4 | 6 |
| **Nodal status** | N0 | 8 |
| | N1 | 8 |
| | N2 | 15 |
| **Distant Metastasis** | M0 | 25 |
| | M1 | 6 |
| **pTNM** | II | 9 |
| | III | 10 |
| | IV | 12 |
| **Histological grading** | moderately differentiated | 12 |
| | poorly differentiated | 19 |

*Note.*—pTNM = pathological tumor, node, metastasis

| Table 2. Perfusion Values in Gastric Cancer Compared with Histological Grade |
|----------------------------------|
| **Histological Grade** | Mean | SD | p value |
| Blood Flow (ml/100 g/min) | poorly differentiated | 50.159 | 15.611 | 0.499 |
| | moderately differentiated | 44.119 | 20.180 | |
| Blood Volume (ml/100 g) | poorly differentiated | 7.127 | 4.161 | 0.433 |
| | moderately differentiated | 5.837 | 2.357 | |
| Mean Transit Time (sec) | poorly differentiated | 11.682 | 4.981 | 0.916 |
| | moderately differentiated | 11.903 | 5.786 | |
| Permeability Surface (ml/100 g/min) | poorly differentiated | 16.471 | 9.003 | 0.040 |
| | moderately differentiated | 9.558 | 5.422 | |
| Microvessel Density (per/*400 field) | poorly differentiated | 44.150 | 14.203 | 0.178 |
| | moderately differentiated | 34.900 | 10.875 | |

*Note.*—SD = standard deviation
Enhance medium (Iopromide, Ultravist300; Schering, Berlin, Germany) via the antecubital vein at 4–5 ml/s. The following parameters were used: 10 s for the scan delay from the start of injection; 5 mm slice thickness (reconstruction slice thicknesses were 5 mm and 10 mm); 1 s gantry rotation period with a 1 s temporal resolution; 120 kV, 100 mA and a 60 sec transverse data acquisition period. Next, the data were transferred to a workstation (Advantage Windows 4.0; perfusion 3.0; GE Medical Systems) and analyzed using commercial software. The advantages of the analytical method included a deconvolution for perfusion and blood volume, which demonstrated good temporal resolution and high spatial resolution, while high image noise and limited volume coverage appeared to be its disadvantages.

The abdominal artery was used as a partial-volume averaging correction. Each region of interest, drawn over the tumor by a radiologist section by section, was as large as possible to reduce noise (> 50 pixels) and to almost completely cover the whole lesion, with care to exclude peripheral fat and necrotic area. Maps of tumor blood flow (BF) (ml/100 g/min), blood volume (BV) (ml/100 g), mean transit time (MTT) (sec), and permeability surface (PS) (ml/100 g/min) were calculated automatically for all four sections (with reconstruction slice thickness 5 mm) available for each patient. The same process was repeated.

### Table 3. Perfusion Values in Gastric Cancer Compared with Serosal Involvement

|                     | Serosal Involvement | Mean   | SD     | p value |
|---------------------|---------------------|--------|--------|---------|
| Blood Flow (ml/100 g/min) | –                   | 40.469 | 12.686 | 0.192   |
|                     | +                   | 51.984 | 19.568 |         |
| Blood Volume (ml/100 g)   | –                   | 5.493  | 2.386  | 0.138   |
|                     | +                   | 7.799  | 2.568  |         |
| Mean Transit Time (sec)  | –                   | 11.096 | 5.967  | 0.636   |
|                     | +                   | 12.085 | 5.015  |         |
| Permeability Surface (ml/100g/min) | –                   | 12.075 | 6.089  | 0.365   |
|                     | +                   | 15.213 | 5.015  |         |
| Microvessel Density (per/*400 field) | –                   | 38.300 | 13.573 | 0.551   |
|                     | +                   | 42.450 | 12.421 |         |

### Table 4. Perfusion Values in Gastric Cancer Compared with Distant Metastasis

|                     | Distant Metastasis | Mean   | SD     | p value |
|---------------------|-------------------|--------|--------|---------|
| Blood Flow (ml/100g/min) | –                   | 48.136 | 18.205 | 0.996   |
|                     | +                   | 48.194 | 10.921 |         |
| Blood Volume (ml/100g) | –                   | 6.506  | 2.717  | 0.585   |
|                     | +                   | 7.646  | 4.409  |         |
| Mean Transit Time (sec) | –                   | 12.089 | 5.609  | 0.488   |
|                     | +                   | 10.086 | 2.914  |         |
| Permeability Surface (ml/100g/min) | –                   | 12.927 | 6.089  | 0.322   |
|                     | +                   | 15.213 | 5.015  |         |
| Microvessel Density (per/*400 field) | –                   | 38.300 | 13.573 | 0.551   |
|                     | +                   | 42.450 | 12.421 |         |

### Table 5. Perfusion Values in Gastric Cancer Compared with Lymphatic Metastasis and pTNM

|                     | Lymphatic Metastasis | Coefficient | p value | pTNM | Coefficient | p value |
|---------------------|----------------------|-------------|---------|------|-------------|---------|
| Blood Flow          |                      | 0.146       | 0.433   | –0.114 | 0.549       |
| Blood Volume        |                      | 0.185       | 0.327   | –0.086 | 0.651       |
| Mean Transit Time   |                      | 0.023       | 0.905   | 0.018  | 0.925       |
| Permeability Surface|                      | 0.480       | 0.038   | 0.509  | 0.026       |
| Microvessel Density |                      | –0.146      | 0.440   | –0.132 | 0.487       |

Note. SD = standard deviation, pTNM = pathological tumor node metastasis
in the sections where reconstruction of slice thickness was
10 mm. Moreover, the mean values were recorded for
further study.

Microvessel Staining and Evaluation
All patients were evaluated pathologically for histologic
diagnosis and MVD counting. The MVD was estimated by
immunohistochemical staining of the surgical specimens
with anti-CD34 monoclonal antibody (Dako, Copenhagen
Denmark) (12).

The criteria for vessel counting were previously
established by Weidner et al. (13). Any single brown-
staining endothelial cell or small clusters of brown-staining
endothelial cells, with or without a lumen, are clearly
separated from its adjacent microvessels, tumor cells, and
other connective tissue elements considered as being
individual vessels. Vessels of a caliber larger than the
approximately eight red blood cells and vessels with a
thick muscular wall were excluded from the final counting.
The MVD counting was performed by a single pathologist.

After screening the areas with intense neovascularized
spots in a low power field (40), the microvessels in the area
with the highest number of discrete microvessels were
counted in a 400x field. Moreover, three separate areas of
intense neovascularization were assessed for each sample
and the mean MVD was calculated for each tumor
evaluated.

Statistical Analysis
The BV, BF, MTT, PS, and MVDs are expressed as the
mean ±standard deviation (SD) and the data were
subjected to a Kolmogorov-Smirnov normality test. All
findings were prospectively analyzed and were found to be
correlated with the clinicopathological results (histological
grading, presence of lymph node metastasis, serosal
involvement, TNM staging, and MVD). The statistical
analyses (t-test and Spearman rank correlation) were
calculated in SPSS 11.5 (SPSS Inc., Chicago, IL). For the
two-tailed tests, p-values less than 0.05 were considered
statistically significant.

RESULTS
The perfusion parameters for gastric cancer in 31
patients (with reconstruction slice thicknesses of 5 and 10
mm) were compared, and revealed no significant differ-
ences (p > 0.3). In this study, the 5 mm reconstruction slice
thickness data was used for all statistical analyses.

The mean perfusion values and MVD for tumors are as
follows: BF (48.14 ±16.46 ml/100 g/min), BV (6.70 ±2.95
ml/100 g), MTT (11.75 ±4.02 sec), and PS (14.17 ±5.23
ml/100 g/min) and MVD (41.7 ±11.53/400x field).
Moreover, the relationship between values and different
histological grades, serosal involvement, distant metastasis,
or lymphatic metastasis, and pTNM are detailed in Tables
2-5. A significant difference exists for the PS value
between patients with or without lymphatic involvement.

**Fig. 1.** Poorly differentiated gastric cancer.
A. Cross section before contrast administration revealed protruding lesion classified as Borrmann I. Regions of interest have been
placed between abdominal aorta and lesion.
B. Corresponding time density curves show arterial and tumor attenuation change with time.
Fig. 1. C. Image calculating blood volume with mean value, 6.71 ml/100 g.
D. Image calculating blood flow with mean value, 73.64 ml/100 g/min.
E. Image calculating mean transit time with mean value, 10.45 sec.
F. Those values of lesion were rather lower; permeability surface (mean, 18.49 ml/100 g/min) appeared to be rather high.
G. This patient had low microvessel density (mean, 21/400 field).
(\(p = 0.038\)), as well as among different histological grades (\(p = 0.04\)) and TNM staging (\(p = 0.026\)). However, the BF, BV, MTT, and MVD of gastric cancer revealed no significant relationship with any clinicopathological features (\(p > 0.05\)) (Figs. 1, 2).

DISCUSSION

Currently, a perfusion CT is calculated by the deconvolution approach, which is based on the theory that immediate enhancement of the tumor is largely due to the presence of the contrast media within the intravascular space and its first-pass to the extravascular space. With the leakage to the extravascular space, the enhancement of the tumors are caused by the contrast media in both the intravascular and extravascular space (10). The deconvolution model has the ability to tolerate greater image noise, is therefore rather well suited to abdominal scans, and is the preferred method for the measurement of low levels of perfusion, which are applicable to gastrocarcinoma (14).

No consensus has been reached regarding optimal scan techniques in the published literature. The first item of controversy and debate is the acquisition time. The majority of the injected contrast media remains intravascular within 40 s (it is also affected by cardiac output and central blood volume); however, a much greater proportion later passes into the extravascular space. Eventually, equilibrium is reached and the blood returns into the intravascular space. The duration of this process lasts around 2 to 4 min (15–17). A perfusion CT scan was performed prospectively in 10 patients with histologically-proven colorectal cancer using different acquisition times (45, 60, and 130 s) by Goh et al. (18). No significant difference was found for BF, BV, or MTT values between any acquisition times; however, significant differences in PS were found between 45 sec and 65 or 130 sec. By measuring the attenuation change within the input artery and tumor, an IRF (input response function) curve can be derived. The peak of this curve is regarded as BF, while BV is represented by the area under the curve. As a result, different acquisition times do not drastically affect these three values since the shape of the curve is fixed. Although the radiation dose in a perfusion CT scan is around 700 mGy (70% of abdominal CT), the extra 2 min dose may be harmful to the patient and efforts should be taken to minimize the dose. Furthermore, a long acquisition time can lead to respiratory motion in an abdominal scan. When taking all of these elements into account, we determined that the 60 sec acquisition time be the most appropriate for our study.

The 60 sec acquisition time would be very difficult to diminish respiratory artifacts. It is most unlikely that the patients will suspend respiration for 60 sec. Furthermore, patients who suspend their breathing will often exhale, which will lead to more motion artifacts and the temptation to take a deep breath when experiencing the “hot flush” associated with a rapid bolus of contrast medium will interrupt the perfusion scanning. Therefore, a quiet respiration was requested during the scan, with patients in the prone position and fixed with a waistline to reduce the
Fig. 2. C. Image calculating blood volume with mean value, 4.59 ml/100 g.
D. Image calculating blood flow with mean value, 100.45 ml/100 g/min.
E. Image calculating mean transit time with mean value, 4.1 sec.
F. Lesion values were lower; permeability surface (mean, 21.93 ml/100 g/min) was relatively high.
G. Patient had high microvessel density (mean, 61/*400 field).
extension of respiration (14).

Pathological TNM staging, histological grading, serosal involvement, lymphatic metastasis, and MVD have been identified as important predictors of the prognosis resulting from gastric cancer in our study (19 – 20). Moreover, pTNM is the conventional prognostic index as it reflects the depth of invasion as well as lymphatic or distal metastasis (3). Tumor outcome is determined by tumor size, extent, stage, and biological behavior and is largely described according to its histological grade. Recent studies have acknowledged that the lymphatic metastasis status is critical in the prognosis of gastric cancer. The mortality of patients with lymphatic metastasis is 3.92x greater than patients without lymphatic metastasis. Angiogenesis is a highly complex phenomenon that is essential for the growth of solid tumors, hence permitting rapid tumor growth and increased potential for tumor metastasis. Furthermore, angiogenesis is a significant predictor of prognosis and hematogenous metastasis in patients with gastric cancer. MVD is currently applied as an indicator of tumor angiogenesis, and it has further been demonstrated that, in some tumors, up to 15% of tumor blood vessels demonstrate the presence of cancer cells in the lumen (21). It is proposed that these small, leaky vessels allow tumor cells to reach the circulatory system, thus increasing the probability of metastasis. The results of a multiple elements analysis in breast cancer, indicated that MVD plays a more important role in predicting invasion and metastases than other clinical indicators. Also, several studies have shown a positive statistical correlation between MVD and metastasis in other solid tumors such as in the lung, uterus, cervix, and prostate. However, the relationship is controversial in gastric cancer (5, 22 – 24).

According to the results of this study, there is a significant difference for the PS value between patients with and without lymphatic involvement. Moreover, there is also a significant difference between different histological grades and TNM stages, while BF, BV, MTT, and MVD revealed no significant correlation with clinicopathological findings for gastric cancer.

Permeability surface represents the transmission rate of contrast media from capillary endothelium to interstitial space, reflects the integrity of endothelial cells and permeability of vessels. It is known that tumor capillaries, in general, have wide inter-endothelial junctions, a large number of fenestrate and transendothelial channels, and discontinuous or absent basement membrane. Compared to normal vessels, they are more easily penetrated by large particles, including tumor cells. This whole process often happens along with an inflammatory reaction that accelerates permeability changes (22, 25). Previous reports have put too much emphasis on blood flow of the tumor rather than the functional differences compared to normal vessels-capillary permeability, which appears to be of value in grading of cerebral glioma and lung cancer (13, 26). We believe PS to be an indicator of prognosis in gastric cancer, warranting further study in larger cohort of patients.

There is no significant difference in the BF, BV, MTT and MVD between patients with and without lymphatic involvement, but also with different histological grades and TNM staging. The reasons for this may be as follows: First, this may be due to the small size of the study population, which contained many patients with poorly differentiated carcinoma, which perhaps causes some statistical bias. Second, elevated tissue pressure present at the center of such tumors have caused the lumen and resulted in the underestimation of the MVD (3). Third, it has been suggested by Sahani et al. (10) that angiogenesis stimulates the opening of significant numbers of arteriovenous shunts, rather than producing a new vascular supply (10).

Anything above may affect the result of BF, BV and MTT values. Moreover, different tumors have different pathological features. Regional cerebral blood volume is closely related to the grading of glioma (27). Fourth, tumor vessels are structurally and functionally abnormal, with uneven diameters, increased length and tortuosity, multiple arteriovenous shunts, and loss of physiological regulation of blood flow. The distribution of tumor vessels is uneven, with a large amount in the vascular area and a small amount in necrotic region. Because MVD is a direct technique has a significant shortcoming as it depends on the availability of postoperative tissue or biopsy materials. Also, different areas will present different densities.

Additionally, a gastric ulcer is associated with cancer, thus complicating accurate calculation (28). Fifth, there is the possibility that MVD acts as an indicator of angiogenesis correlates hematogeneous metastasis.

Several limitations exist in our study. First, as the size of the study population was too small, no estimation of the absolute value of PS data could be provided for under a clinical analysis. Second, too many patients with poorly differentiated carcinoma lead to statistic bias. Third, the lack of control group in the study is another limitation, the normal gastric wall is more likely to be too thin for us to achieve perfusion CT values. Fourth, a respiratory artifact is something hard to overcome, especially for a 60 sec free breathing scan. It may interfere with the results. Fifth, extraradiation dose of CT perfusion is harmful and we should minimize it. It has been reported that MRI could aid in optimizing treatments, categorizing lesions, and influencing patient care in brain tumors (26), which might be a hint for the further investigation in gastrointestinal
system. There is still a long way to go.

In summary, perfusion CT is a reproducible, objective, and feasible imaging strategy for the evaluation of oncology. Furthermore, the analysis of perfusion CT in gastric cancer (especially for the PS value), might be a helpful prognostic indicator, or as being useful for predicting the response to clinical treatment.

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