MEMS inductor fabrication and emerging applications in power electronics and neurotechnologies

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Abstract
MEMS inductors are used in a wide range of applications in micro- and nanotechnology, including RF MEMS, sensors, power electronics, and Bio-MEMS. Fabrication technologies set the boundary conditions for inductor design and their electrical and mechanical performance. This review provides a comprehensive overview of state-of-the-art MEMS technologies for inductor fabrication, presents recent advances in 3D additive fabrication technologies, and discusses the challenges and opportunities of MEMS inductors for two emerging applications, namely, integrated power electronics and neurotechnologies. Among the four top-down MEMS fabrication approaches, 3D surface micromachining and through-substrate-via (TSV) fabrication technology have been intensively studied to fabricate 3D inductors such as solenoid and toroid in-substrate TSV inductors. While 3D inductors are preferred for their high-quality factor, high power density, and low parasitic capacitance, in-substrate TSV inductors offer an additional unique advantage for 3D system integration and efficient thermal dissipation. These features make in-substrate TSV inductors promising to achieve the ultimate goal of monolithically integrated power converters. From another perspective, 3D bottom-up additive techniques such as ice lithography have great potential for fabricating inductors with geometries and specifications that are very challenging to achieve with established MEMS technologies. Finally, we discuss inspiring and emerging research opportunities for MEMS inductors.

Introduction
Transistors, capacitors, resistors, and inductors are the four fundamental components of electrical circuits. The importance of each component to science, engineering, and society is paramount. In this review, we focus on inductors such as solenoid, toroidal, and spiral inductors, coils, and transformers. For the first time, we review microelectromechanical systems (MEMS) inductor fabrication technologies, which serve as the foundation of our literature search. We analyze and process the literature to give the reader a comprehensive overview of MEMS inductor fabrication technologies and emerging applications. In “MEMS fabrication of inductors” section, we group MEMS inductors into four categories and present the technical terminology used for MEMS inductor fabrication. In the same section, we review four different fabrication technologies and highlight their advantages for their target applications.

Most reported microinductors were made with established top-down or subtractive MEMS microfabrication and nanofabrication methods such as lithography, etching, electroplating, and thin-film deposition processes. Owing to important and creative MEMS fabrication technology innovations, additive microfabrication, and nanofabrication methods have emerged over the past 10 years. In “Emerging 3D nanofabrication technologies”
section, we review important emerging nanoscale fabrication methods that have been used for MEMS inductor fabrication or hold promise for becoming new versatile tools for microinductor and nanoinductor production. An overview section maps the emerging technologies, and four promising technologies are presented.

In addition to reviewing inductor fabrication technologies, our literature study and analysis categorize MEMS inductor applications into four groups: radio frequency (RF) MEMS, wireless and sensors, power electronics, and biomedical MEMS. RF MEMS and power electronics applications of MEMS inductors account for over 300 studies. Excellent reviews on RF applications exist. However, there are no reviews on the other applications. Thus, we reasoned that it is important to review the power electronics applications, as presented in “Power electronics applications” section. The number of studies on power inductors for power converters has increased steadily following the rapid growth of smart electronic devices, wearables, lighting, and the Internet of things (IoT).

In the last 10 years, the usage of MEMS inductors for biomedical applications has been explored, and we observed an increasing number of publications. In “Biomedical and neurotechnology applications” section, we review a subset of the biomedical applications, which is an emerging field of neurotechnology. Neurotechnology research is substantially supported by the BRAIN Initiative, which focuses on the development of cutting-edge neurotechnologies for science and medicine. Here, we review electrifying new developments in magnetic stimulation of the brain using MEMS coils, which might outperform the well-established electrical stimulation. We discuss important challenges and research opportunities addressing societal challenges.

**MEMS fabrication of inductors**

**Overview**

MEMS inductors consist of three parts: (i) conductive windings, (ii) insulators, and (iii) a core. First, conductive windings are used to carry currents, thus producing magnetic flux. They are made of electrically conductive metals, e.g., copper (Cu), and are fabricated by deposition techniques such as electrodeposition or sputtering. Second, insulators are used to provide electrical isolation between adjacent conductor windings and between windings and the underlying substrate. Here, insulators are dielectric thin films such as silicon oxide (SiO₂), aluminum oxide (Al₂O₃), or silicon nitride (Si₃N₄). The selection of dielectric materials and deposition techniques is performed carefully based on the required isolation level and processing temperature. Third, MEMS inductor cores refer to the material in the magnetic flux path. Inductor cores can be made of either magnetic materials such as iron or ferrite or magnetic materials that come in a variety of shapes, such as magnetic thin films or bar shapes. Innovatively, magnetic cores are also placed around the windings.

MEMS inductors are categorized into four groups based on the shape of the conductor windings and their position relative to the substrate: (i) 2D on-substrate inductors, (ii) 3D on-substrate inductors, (iii) 2D in-substrate inductors,
and (iv) 3D in-substrate inductors. Figure 2 shows 3D illustrations of the MEMS inductors of these four groups, including 2D on-substrate spiral and racetrack inductors (Fig. 2a, b), a 3D on-substrate solenoidal inductor (Fig. 2c), a 2D in-substrate spiral inductor (Fig. 2d), and a 3D in-substrate toroidal inductor (Fig. 2e). Table 1 summarizes these fabrication technologies, applications, merits, and limitations corresponding to inductors in these four inductor groups.

The four inductor categories are realized by different fabrication technologies, which play an essential role in MEMS inductor technology development. They determine an inductor’s physical dimensions and construction materials; therefore, the fabrication process greatly influences the inductor properties. The generic properties of MEMS inductors are the quality factor, inductance density, and operating frequency. Furthermore, there are important parameters for MEMS inductors, such as the EMI, breakdown voltage, leakage current, and parasitic capacitance.

We classify inductor fabrication technologies into four categories: 2D micromachining, 3D micromachining, through-substrate via (TSV)-based technology, and other technologies such as wire bonding, 3D printing, and self-assembly approaches. Figure 3 summarizes the development of MEMS inductor fabrication technologies since 1990.

2D surface micromachining

The first fabrication technology for MEMS inductor fabrication is 2D surface micromachining (Fig. 4). The development of surface micromachined inductors dates back to the early 1990s, with a number of foundational studies by Allen et al. on meander magnetic core inductors, Sullivan et al. on racetrack inductors, and Sato et al. on strip line inductors. They are widely used in many applications because of their compact size, process simplicity, and CMOS compatibility. Tremendous efforts have been invested towards design optimization and building physical models for 2D planar inductors, providing a comprehensive understanding of how physical parameters and high-frequency eddy currents affect inductor performance. Here, we focus on fabrication advances in winding deposition technology and methods to enhance the electrical isolation between a winding and the substrate to minimize unwanted parasitic capacitance and substrate losses.
| Fabrication technology | Geometry | Year | Key features | Application | Developments and trends |
|------------------------|----------|------|--------------|-------------|------------------------|
| 2D surface micromachining | Planar spiral | On-chip square spiral. | RF | Winding layout optimization \(^{152}\), winding density improvement, substrate isolation by suspended windings\(^{17,25}\), and buried oxide\(^{14,15}\). |
| 2D surface micromachining | Racetrack | 2012\(^{23,53}\) | Substrate-embedded racetrack windings, nanolaminated sputtered Co-Zr-O magnetic core. | Power | Winding density improvement by high-aspect-ratio (high-AR) winding\(^{10-12}\), thin-film nanolaminated magnetic core\(^{27,134}\), axial anisotropy implementation\(^{26,135}\). |
| 3D surface micromachining | Solenoid | 2005\(^{56}\) | Polymer-core windings, high profile. | Power | Nanolaminated core implementation\(^{38}\). |
| 3D surface micromachining | Solenoid | 2008\(^{36}\) | Low profile, CMOS-compatible integration. | Power | Substrate electrical isolation by suspended windings\(^{34,35}\), substrate-embedded windings\(^{157,158}\), thin-film nanolaminated magnetic core\(^{7,18}\), low-loss magnetic materials\(^{5,53,101,102}\), vertical laminated magnetic core\(^{38}\). |
| 3D surface micromachining | Toroidal | 2013\(^{159}\) | Polymer-core windings, high profile, nanolaminated core. | Power | Substrate-embedded windings\(^{157}\), radical anisotropy implementation for toroidal inductor\(^{160}\). |
| TSV fabrication processes | Spiral | 2011\(^{51}\) | Low profile, substrate-embedded spiral windings, Si core, through-substrate interconnections. | Power, wireless | Through-silicon windings, double-sided embedded windings\(^{161}\), stacked substrate\(^{36}\), magnetic core integration. |
| TSV fabrication processes | Solenoid, Toroidal | 2018\(^{37}\) | Void-free high-AR TSVs, substrate-isolation by suspended windings. | Power | Hollow Cu TSVs\(^{65,161}\), magnetic self-assembly for TSV fabrication\(^{164}\), void-free high-AR TSV filling\(^{65,166}\), magnetic core integration\(^{33,106,168}\). |
| Other processes | Solenoid | 2019\(^{34}\) | 3D-printed vertical solenoid, selective silver deposition. | RF | Direct writing by femtosecond laser\(^{169}\). |
| Other processes | 3D spiral | 2015\(^{53}\) | Self-rolled-up membrane. | RF, BioMEMS | Magnetic core integration using magnetic liquid\(^{59}\), multilayer transformers\(^{70}\). |
| Other processes | Solenoid | 2010\(^{58}\) | Wire-bond vertical solenoid, automatic wire bonder. | RF, sensing | Horizontal toroidal winding\(^{69}\), soft ferrite core integration\(^{69}\). |
First, developments in winding technology have been driven towards the creation of compact, thick, high-aspect-ratio windings. Resist mold electrodeposition is a powerful method for fabricating 2D planar inductor windings; thus, high-aspect-ratio lithography processes are necessary. Anthony et al.\textsuperscript{10} studied high-aspect-ratio THB-151N resist molds for Cu electrodeposition. An aspect ratio of 1:17 was achieved, resulting in the successful fabrication of 80-µm-thick, 25-µm-wide, and 5-µm-spacing spiral inductor windings. They showed that the direct current (DC) resistance of 80-µm-thick winding inductors is 42% lower than that of 50-µm-thick winding inductors. In addition, inductors with a 5-µm spacing also have 25% smaller footprints than inductors with a 15-µm spacing. Similar studies on other high-aspect-ratio resist molds can also be found\textsuperscript{11,12}.

Second, another notable improvement in the 2D micromachining process is the fabrication approaches followed to increase winding-substrate isolation to reduce unwanted parasitic capacitance and substrate losses\textsuperscript{13}. There are two approaches. The first approach is to fabricate inductors on a thick isolation layer. A common method to fabricate thick buried oxide islands is to etch deep trenches into Si substrates followed by a SiO\textsubscript{2} deposition step either by PECVD\textsuperscript{14,15} or thermal oxidation\textsuperscript{16}. For example, the quality factor increased from 3.5 at 4.6 GHz to 7 at 7 GHz for inductors fabricated on 2-µm-thick and 20-µm-thick oxide layers, respectively\textsuperscript{16}.

![Fig. 3 Number of publications on MEMS inductor fabrication technologies over time. Please see supplementary material for source data](image_url)

![Fig. 4 2D micromachined spiral inductors. Suspended windings and air gaps made by a removing a sacrificial layer\textsuperscript{25} (Copyright IEEE 2004) and b etching the underlying substrate\textsuperscript{17} (Copyright MDPI 2011). c 2D micromachined racetrack inductor with a magnetic thin-film core\textsuperscript{27} (Copyright IEEE 2013)](image_url)
The second approach is to induce an air gap between the winding conductors and substrate, resulting in suspended windings\(^{17-24}\). This is carried out by removing materials under the winding conductors, for example, by using sacrificial layers\(^{25}\) or by etching the substrate under the inductor windings\(^{18}\). In general, the quality factor and operating frequency increase as a result.

Another approach is to integrate magnetic thin films that act as a shield to reduce eddy currents generated in the underlying substrate. In addition, a magnetic thin-film core is a key feature to achieve a high inductance density, which is desired in applications such as switched-mode power supplies (SMPSs)\(^{6}\). A similar design of windings and thin-film cores can be seen in racetrack inductors\(^{26}\).

Figure 4c shows an elegant fabrication process of the racetrack inductor\(^{27}\). The process has four steps: (i) depositing the bottom magnetic thin film, (ii) depositing the 1st insulator layer and Cu windings, (iii) depositing the 2nd insulator layer, and (vi) depositing the top magnetic thin film. Similar fabrication approaches can be found for other racetrack power inductors\(^{28,29}\). Although the winding structures are similar in most racetrack inductors, innovative variations exist in magnetic thin-film technology. For example, because racetrack inductors are mainly used for power conversion, developments have focused on discovering new magnetic materials and new core structures for high permeability and low core losses. Recent developments in magnetic materials are summarized in references\(^{30,31}\).

**3D Surface Micromachining**

The second fabrication technology is 3D surface micromachining technology, which has been developed for fabricating 3D inductors such as solenoid and toroidal inductors. There are three groups of on-substrate 3D micromachined inductors: low-profile air-core inductors (Fig. 5a), low-profile magnetic-core inductors (Fig. 5b), and tall-profile inductors (Fig. 5c).

3D micromachined processes for low-profile inductors typically involve several resist-mold electroplating and sacrificial layers to construct multiple levels of conductors. Zia et al.\(^{32}\) reported a 110-µm-tall domed-shaped solenoidal inductor for RF applications, as shown in Fig. 5a. The key aspect is the 3D patterning of Cu windings on dome-shaped resist molds created by resist reflowing. The fabricated 110-µm-tall inductor has an inductance of 2.5 nH with a quality factor of 25 at 33 GHz. Small-inductance and low-profile 3D micromachined air-core solenoidal inductors are used for RF applications\(^{30,33}\). In some cases\(^{34,35}\), suspending inductor windings improves the high-frequency quality factor and frequency of 3D micromachined solenoidal inductors. The underlying substrate material is etched to produce an air gap between the windings and substrate, thus reducing unwanted parasitic capacitance and substrate effects. A similar approach is also found in the 2D micromachining processing of 2D inductors, as mentioned above.

For high-frequency power conversion, a higher inductance density is needed. Two approaches exist: either integrate the magnetic core between the 3D windings\(^{36,37}\) or increase the inductor height, because the inductance of the solenoidal and toroidal inductors is proportional to the core cross-sectional area. For the first approach, an example of a low-profile 3D magnetic-core inductor is shown in Fig. 5b. Michael et al.\(^{37}\) reported 150-µm-tall solenoid inductors embedded with a sputtered...
nolanlaminated magnetic core for high-frequency power conversion. An inductance of up to 500 nH was achieved with a stack of 20 layers alternating between an 80-nm-thick Co–Zr–Ta magnetic layer and a 4-nm-thick Al2O3 layer. The second approach is to increase the inductor cross-sectional area. For example, SU-8 technology was utilized to fabricate 3D inductors with mm-tall, high-aspect-ratio vertical conductors. In these studies, polymer-encapsulated vertical pillars were used as supports for subsequent Cu electroplating to form inductor vertical conductors. Figure 5c illustrates a process reported by Kim et al., which starts with the fabrication of SU-8 support pillars followed by seed layer sputtering and Cu electroplating to form the bottom and vertical windings. Next, a premade laminated magnetic core is inserted on an insulating film between vertical solenoidal windings. SU-8 pellets are then cast on a substrate to partially cover the Cu windings and magnetic core. Last, an electroplating mold is lithographically patterned, followed by top Cu winding electrodeposition. On-chip solenoid inductors of 1-mm-tall, 200-µm-diameter vertical vias were successfully demonstrated. Because of the mm-tall profile, these inductors are suitable for high-power applications where the device profile is not a limiting factor. Alternatively, windings can be embedded into the substrate to construct tall 3D inductors for high inductance.

Through-substrate-via fabrication process

TSV technology was originally developed as a packaging solution for the vertical integration of multiple chips in the third dimension. This packaging approach uses chips, or so-called interposers, consisting of vertical interconnections and redistribution layers (RDLs) on both substrate sides to pass electrical signals between stacked chips, thus substantially increasing the interconnection density. TSV technology was adapted for MEMS inductor fabrication in the mid-2000s, with studies on both 2D spiral inductors and 3D solenoid inductors.

In the last 10 years, substantial developments have been made in all four aspects of TSV fabrication technology, including (i) TSV hole drilling, (ii) dielectric insulator deposition, (iii) TSV conductor deposition, and (iv) substrate planarization and routing conductor patterning.

First, TSV hole fabrication technologies can be categorized into four main methods: physical ablation (laser drilling and sand blasting), lithographically based processes (photosensitive glass substrate), wet etching (metal-assisted wet etching), and plasma etching (deep reactive ion etching (DRIE) Bosch Si etching, SiO2 dry etching). Details on the advantages and disadvantages of each method are presented in reference. According to reference, DRIE Si etching using the Bosch process is by far the most versatile technique, providing excellent control over TSV dimensions, such as TSV spacings (10–15 µm) and ultrahigh aspect ratios (AR = 50–100).

The second step is dielectric insulator deposition. The dielectric constant, thickness, and conformality are important properties that have a large influence on the parasitic capacitance, breakdown voltage, and cross-talk between TSVs. The insulator deposition technology needs to be carefully considered. Deposition technologies include plasma-enhanced vapor deposition (PECVD) SiO2, atomic layer deposition (ALD) SiO2 and Al2O3, and polymers such as SU-8, spin-coated or PVD-growth polyimide (PI), polybenzoxazole (PBO), or benzocyclobutene (BCB). A summary of important characteristics such as the conformality, processing temperature, and dielectric properties of these materials and the

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Fig. 6 A TSV-based process for fabricating a 3D in-substrate toroidal inductor (Copyright Springer Nature 2018). a Fabricated inductors, including air-core toroidal inductors, a toroidal transformer, a solenoid inductor, a spiral inductor, and an inductor with an arbitrary “DTU” core shape. b Four main steps for fabricating the toroidal inductor (Copyright IEEE 2018)
corresponding deposition technologies are presented in reference48.

The third step is vertical via conductor fabrication. Electrodeposition is a widely used technology for TSV fabrication, in addition to other methods such as the magnetic assembly of microwires49. There are two approaches for TSV electrodeposition: electroless electroplating for hollow TSVs, top-down electroplating for half-through TSVs, and bottom-up electroplating for TSVs50. Electroless plating offers great conformality, but it is time-consuming and requires a conformally coated seed layer on the TSV sidewalls. It is often used for fabricating hollow TSVs. Top-down electroplating is the most developed technique for TSV fabrication. It is most suited for fabricating 2D in-substrate inductors51–56. To realize TSVs, extra steps of substrate back-lapping and planarization are needed. Bottom-up electroplating enables the fabrication of tall, high-aspect-ratio, solid TSVs, at the cost of a long plating time. This technique is best used in fabricating inductors with thick windings, as required to handle high DC and AC currents, such as in power electronic applications. For example, Wang et al.43 demonstrated TSV spiral inductors with 200-μm-wide TSVs that successfully carried up to 5A of DC current with a DC resistance of 23 mΩ. Examples of 3D TSV-based power inductors can be found in references57,58. The last steps in the TSV fabrication process are substrate planarization and routing conductor patterning.

Next, we discuss a representative TSV-based fabrication process for 3D in-substrate inductors for VHF power conversion. Figure 6a shows SEM micrographs of fabricated inductors and transformers, including toroidal inductors, a toroidal transformer, a solenoid inductor, a spiral inductor, and a “DTU” inductor with an arbitrary core shape. These inductors have unique features, such as in-substrate suspended windings that are held by five Si fixtures. The windings are separated from the Si substrate by an air gap of 300 μm, thus significantly reducing unwanted substrate effects. As shown in Fig. 6b, there are four main steps in the fabrication process: (i) TSV hole etching by DRIE and insulation layer deposition, including ALD Al2O3 and PECVD SiO2. The inductor core shape is defined by the fixture trench, as depicted in Fig. 6c. (ii) TSV bottom-up electroplating and winding patterning. (iii) Creation of a core-etching mask. (iv) Selective removal of a silicon core via isotropic dry etching by inductively coupled plasma (ICP) silicon etching, leaving Si fixtures protected by a layer of Al2O3 deposited on the fixture trench in step 1. More details of the process parameters can be found in reference57. This process has a unique ability to precisely remove an unwanted Si core to boost the inductor performance. The hollow air core, which can be fabricated in arbitrary core shapes, can be subsequently filled by magnetic particle composites to realize magnetic-core inductors with a higher inductance density59. The process is CMOS-compatible and scalable to a wide range of TSV diameters (30–50 μm) and substrate thicknesses (280–500 μm). A similar approach was also presented in recent studies on the in-substrate 3D solenoidal inductor60.

Other processes: self-assembly processes and bonding techniques

Self-assembly fabricates MEMS inductors by a post-micromachining step to arrange out-of-plane 2D or 3D inductor windings. An advantage of self-assembled inductors is the simplicity in fabricating complex winding structures without the need for excessive multilayer processing. Self-assembled inductor windings were originally planar conductors that are later released and assembled in a 3D fashion. Several mechanisms have been reported for inductor self-assembly, such as the post release folding process61 (Fig. 7b), plastic deformation magnetic assembly (PDMA)62, and self-rolled-up membrane (S-RUM)63 (Fig. 7a).

Taking the S-RUM process as an example, its self-assembly mechanism is achieved by depositing a bilayer of oppositely strained silicon nitride (SiNc). By etching an e-
beam-evaporated Ge sacrificial layer to release a stack of multilayer thin films, the SiNₓ-Cu layers roll up, forming 3D tubular solenoidal inductors. An additional step to put ferrofluid into a solenoidal core to enhance the inductance density has also been demonstrated. It has been reported that S-RUM tubular inductors have a high inductance density and reduced parasitic substrate effects. Moreover, the Cu thickness is critical for controlling the rolling step; therefore, thin Cu layers are preferred. Inductors with Cu layer thicknesses from 100 to 250 nm have been demonstrated. The same limitation applies to other self-assembly mechanisms that are applicable only for Cu thicknesses from hundreds of nanometers to a few micrometers, which are ideal for low-current applications, such as RFID, RF applications, and transformers for power transfer.

Bonding technologies such as wire bonding and flip-chip bonding are also utilized for inductor fabrication. Wire-bonded inductors use bonded wires to construct 3D windings (Fig. 7c). The main advantages of this approach are the process simplicity and feasibility and the lower manufacturing costs compared to top-down microfabrication processing. Chip-to-chip bonding techniques such as flip-chip bonding could also be used to realize complex inductor windings by bonding chips, such as suspended spiral inductors.

Emerging 3D nanofabrication technologies

“MEMS fabrication of inductors” section reviewed top-down MEMS fabrication for inductor fabrication; in this section, we focus on emerging bottom-up methods. The trend of developing 3D structures using bottom-up fabrication methods has been stimulated by the global demand for environmentally friendly maskless high-resolution fabrication techniques along with the reduced use of hazardous chemicals and materials. Direct ink writing (DIW) is a simple and versatile additive manufacturing (AM) method to produce 3D structures with dimensions above 1 µm. Here, a wide range of materials can be printed by extruding printing materials through a nozzle. In the last 10 years, techniques such as fluidic forced microscopy (FluidFM), two-photon stereolithography (TPS), focused electron beam-induced deposition (FEBID), and ice lithography (IL) have emerged as bottom-up AM methods for high-precision three-dimensional manufacturing, enabling multilevel device prototyping in one printing step. The smallest structures made by these methods are 1 nm in size. Table 2 summarizes the main characteristics of the emerging AM techniques. These techniques have the potential to be employed as cost-effective and time-efficient ways of developing 3D micro- and nanostructures, including 3D microinductors.
Fluidic forced microscopy

FluidFM is a DIW method that takes advantage of the spatial precision of atomic force microscopy (AFM) along with the local ink delivery capability of microfluidics and nanofluidics. Thanks to the advancement of miniaturization technologies, AFM probes with integrated microscopic channels inside the tip enable microscale and nanoscale 3D printing via direct material delivery. The microchanneled cantilevers have a flexible design, and the volumes they can handle are in the femtoliter to picoliter range. FluidFM allows accurate printing on existing structures. The inks for the FluidFM deposition method are often composed of particulate and polymeric materials that are suspended or dissolved in a liquid solvent and solidify upon extrusion. A wide variety of materials, namely, polymeric, ceramic, metallic, hydrogel, and biomaterials, can be printed using this technique. The viscosity of the printing materials is the most important property to tune for DIW additive deposition. The inks must exhibit pronounced shear-thinning behavior. 3D structures can be fabricated via layer-by-layer printing. In addition, the fabrication of metal structures and electrochemical 3D deposition with FluidFM have been reported. Figure 8a shows a triple helix structure made by FluidFM and illustrates the inductor fabrication capabilities.

Two-photon stereolithography

Two-photon stereolithography (TPS) implements a two-photon polymerization approach for patterning. It uses high-intensity femtosecond laser pulse scanning through a photopolymer or photoresist in a layer-by-layer fashion to create microstructures and nanostructures in a single fabrication step. TPS utilizes the two-photon absorption of near-infrared (NIR) light to excite photosensitive materials. The total energy from two photons is resonant with the energy difference between the ground state and excited state. The TPS photopolymer is transparent in the NIR region; thus, the lasers penetrate deep into the materials and directly induce polymerization inside only the focal volume. The nonlinear two-photon process allows subwavelength fabrication, which is not possible by diffraction-limited stereolithography. Thus, TPS enables the fabrication of structures with dimensions below 100 nm.

For selected TPS processes, negative-tone photoresists are used as photosensitive materials. Their solubility decreases with exposure to the dose of photons due to the cross-linking of monomers or oligomers in the photoresist. Free-radical-based or cation-based intermediates are applied to excite cross-linking, which can be initiated, respectively, by a photoinitiator or a photoinitiator-photon-acid generator. Different polymeric materials and their composites, depending on the desired functionalities, are used for TPS. For example, to develop conductive structures, carbon nanotube (CNT)-based polymer composites have been employed. Furthermore, Ag and Au salt and photoresist composites have been reported for metal deposition. TPS has many applications, e.g., the development of microfluidics, sensors, actuators, microbots, and biomedical devices. Ha et al. reported 3D microcoils employing TPS using a dual-stage femtosecond laser scanning process. The coil was made of a hybrid material consisting of a polymer and a “metal-coatable polymer”. Electroless plating of silver was performed to achieve selective metallization of the metal-coatable polymer microstructure. The 3D microcoil with five turns, a diameter of 200 μm and a height of 60 μm can be operated at 25.4 GHz.
Focused electron beam induced deposition (FEBID)

Based on electron-gas interactions, FEBID is a direct-write approach for the fabrication of 2D and 3D nanostructures. During FEBID, an electron beam (e-beam) is scanned over a sample in the presence of precursor gases to deposit patterns of materials onto a substrate. Scanning electron microscope (SEM), along with a gas injection system, is employed for the FEBID method, and organic precursor gases are used as the printing materials. In FEBID, the material deposition (growth) process depends on several precursor-specific aspects, namely, the vapor pressure of the precursor, the adsorption characteristics of the precursor molecules, and their stability under adsorption. Under continuous e-beam exposure, the surface physisorbed or chemisorbed precursor molecules are dissociated. The low-energy secondary electrons and backscattered electrons generated by the primary electrons trigger the electron-induced dissociation process. FEBID is particularly appropriate for microscale and nanoscale structure manufacturing since precursor molecules are small and e-beams can be focused onto spots with diameters varying from micrometers down to the angstrom level. As examples, SEM images of a 3D magnetic double-loop nanospiral and Moebius strip with a triangular cross section and individual wire dimensions of approximately 25 nm are illustrated in Fig. 8c.

Taking advantage of the organometallic precursors designed for chemical vapor deposition, FEBID deposits metallic, superconducting alloys and intermetallic compounds and metamaterials, such as silver (Ag), gold (Au), platinum (Pt), iron (Fe), tungsten (W), cobalt (Co), and ferrocobalt (Co3Fe) alloys. It enables a high degree of miniaturization that opens the way for a wide variety of applications. A purity of the as-deposited Au, Co, Fe, Si of 94–100%, Ag of ~75% and W of 66% has been reported for FEBID. However, due to incomplete dissociation of the precursors, deposition from standard precursors, such as tungsten hexacarbonyl (W(CO)6), copper (II) hexafluoroacetylacetonate hydrate (Cu(hfac)2), and dimethyl-(1,1,1-trifluoro-2,4-pentandionato) gold (III) (Me2Au(tfac)), could result in deposition with a high carbon content. Therefore, a postdeposition purification process is developed to reduce contaminants by annealing in a reducing 98% N2 and 2% H2 atmosphere at elevated temperatures. For example, the purity of as-deposited ruthenium (Ru) was increased from 23 to 83% after postdeposition annealing at 300 °C.

Ice lithography

IL is a direct-write technique that uses electron-solid interaction principles for nanoscale and microscale fabrication. During the IL process, organic precursor gas is condensed at cryogenic temperatures on the substrate under a vacuum to create an organic ice resist layer, and then a high-energy focused e-beam is used for cross-linking. Figure 9a summarizes the IL process. The e-beam cross-link condenses organic ice to form a large molecule network. Thereafter, excess materials are removed by an evaporation step. Layer-by-layer deposition enables the printing of 3D structures. For the IL process, the focused electron energy is efficiently injected into the organic ice layer. Thus, in comparison to FEBID, IL is 1000 times faster. Moreover, also true for FEBID, the IL process can be applied to substrates with complex geometries. A wide variety of precursors can be patterned by employing IL, considering the formation of an ice resist at cryogenic temperatures. In the case of highly impure and contaminated deposits, similar to FEBID, postdeposition purification processes can be added.

IL can pattern metals; here, the “lift-off” approaches were adapted to dissolve the ice layer. For example, the manufacturing of a rectangular metallic cap on the pyramidal tip of a standard atomic force microscope cantilever is presented (Fig. 9b). Moreover, Au-Ti wires (0.5-μm wide and 300-μm long) with bonding pads are demonstrated on a microcantilever (Fig. 9c). An IL-patterned metallic layer on fragile support structures, where conventional techniques cannot be performed. A palladium (Pd) metallic triangular-shaped pattern with features below 10 nm on a fragile free-standing Si3N4 membrane (Fig. 9d) has also been presented. Elsukova et al. reported the use of a transmission electron microscope as a source of e-beam, which minimizes the influence of instrumental limitations, and showed that the onset dose of organic ice resists correlates with the inverse molecular weight of the organic compound. Continuous parallel lines down to 4.5 nm have been fabricated using a 0.4 pA beam current with frozen octane (C8H18), as presented in Fig. 9f. Furthermore, a 3D Ag-layered pyramidal structure (Fig. 9f) has been reported, where a water ice resist, which acts as a positive-tone resist, was utilized for patterning. Ice lithography is a suitable candidate for developing ultraminiaturized microscale and nanoscale inductors in 2D and 3D forms for a wide range of applications due to its ability to produce fine features in fewer steps. We are currently developing IL to fabricate microinductors.

Power electronics applications

Power supply in package (PwrSiP) and power supply on chip (PwrSoC)

Power supplies play an essential role in all electronic devices. For example, they convert alternating current (AC) signals to direct current (DC) signals. In modern devices where space is strictly limited, including consumer electronic products, light-emitting diode (LED) lighting, wearables, implantable electronics, and the Internet of things (IoT), the miniaturization of power supplies has become a prime interest for future power supply generation. Monolithic integration is the ultimate...
solution to realize highly miniaturized power supplies while achieving superior performance in efficiency and power density. These integrated power supplies are the so-called power supply in package (PwrSiP) and power supply on chip (PwrSoC). Figure 10 illustrates a timeline overview of the notable developments of PwrSoC and PwrSiP.

In fact, in switched-mode power supplies (SMPSs), which are the most widely used power supply technology today, passive components such as inductors and transformers are essential, but they are often the most lossy and bulky components. Switching at higher frequencies allows using smaller inductors. For example, it was predicted that the target switching frequencies for PwrSiP and PwrSoC are at high frequencies (1–30 MHz) and very high frequencies (above 30 MHz), respectively. Previous reviews cover technology trends, specifications, target applications, and enabling technologies for PwrSoC. While other aspects of PwrSoC technology have greatly advanced, such as CMOS integration technologies for active components (e.g., high band-gap GaN, SiC FETs), gate drivers and controllers, and efficient topologies, integrated passive technology and 3D packaging technology remain technology gaps to overcome. Here, we discuss these two topics: (i) MEMS power inductor technology.
for PwrSoC and (ii) MEMS–CMOS integration and packaging technologies of SMPS in relation to MEMS inductor fabrication.

MEMS inductors for PwrSiP and PwrSoC

First, MEMS inductors offer unique characteristics to be used in PwrSiP and PwrSoC applications thanks to the unique advantage of MEMS-CMOS integration. In addition to fundamental properties such as the quality factor and inductance, power MEMS inductors are required to have a sufficient current handling capability (100 mA to 3 A), low electromagnetic interference (EMI), low parasitic capacitance, etc. We summarize the electrical performance of state-of-the-art power MEMS inductors in Fig. 11. First, Fig. 11a presents the frequency-dependent quality factor versus the operating frequency. The presented inductor types have been demonstrated for power electronic applications in the frequency range of interest from 100 kHz to 30 MHz. While other groups of MEMS inductors cover a wide range of $Q$ and frequency, 3D in-Si toroidal inductors stand out, with both a high quality factor ($Q$) and high frequency.

**Fig. 10** Overview of the timeline of notable developments of PwrSoC and PwrSiP using MEMS inductors. Copyright IEEE 2000, 2011, 2013, 2015, 2016, 2017, 2018, 2019

**Fig. 11** Characteristics of MEMS inductors that are used in power converters. a Quality factor versus frequency. b Inductance density versus a figure of merit ($FOM = \sqrt{Q_{DC} \cdot Q_{AC}}/V$)
Table 3  Specifications of notable integrated power supplies using MEMS inductors, as presented in Fig. 10

| Study          | Year | Inductor @ Core material                  | Packaging         | Converter specifications |
|----------------|------|------------------------------------------|-------------------|--------------------------|
| Nakazawa et al.173 | 2000 | On-sub spiral @ CoHfTaPd                 | Integrated on IC  | $V_{in} - V_{out}$ ($V_{DC}$) | Freq. (MHz) | Eff. (%) | $P_{den}$ (W/cm²) | $P_{den}$ (W/cm³) |
| Jia et al.174    | 2011 | Wire bond @ ferrite                      | Wire bond         | 5–3                      | 3           | 80       | 0.178            | 56               |
| Wang et al.106   | 2011 | In-sub TSV spiral @ NiZn                 | 3D, stacked, TSV interposer | 5–2.2               | 5           | 52       | 0.371            | –                |
| Wang et al.175   | 2013 | racetrack @ ferrite                      | Co-packaged, wire bond | 5–0.5              | 40          | 78       | 0.46             | 425              |
| Sturcken et al.104| 2013 | Racetrack @ Ni45Fe55                     | 2.5D, interposer, wire bond | 1.8–1.2            | 100         | 71       | 1.89             | 41.7              |
| Fang et al.176   | 2015 | In-sub TSV spiral @ ferrite              | 3D, stacked, interposer | 110 $V_{AC} - 70 V_{DC}$ | 5           | 73       | 0.175            | 175              |
| Lee et al.177    | 2016 | On-sub spiral @ air                      | On-sub CMOS-integrated | 2.2–1.2           | 500         | 76       | 0.76             | 115              |
| Krishnamurthy et al.103 | 2017 | On-sub 3D solenoid @ laminated Co-based amorphous | On-sub CMOS-integrated | 1.5–1.2           | 100         | 84       | 1.17             | 234              |
| Li et al.178     | 2017 | In-sub TSV spiral @ NiZn                 | 3D, stacked, TSV interposer | 3.6–1.8            | 6           | 83       | 12               | 144.5             |
| Ding et al.179   | 2018 | In-sub TSV spiral @ ferrite              | 3D, stacked, TSV interposer | 130–70            | 5           | 69       | 1.36             | 13.5              |
| Renz et al.180   | 2019 | On-sub spiral @ air                      | On-sub CMOS-integrated | 4.5–1.8            | 475         | 85       | 0.0054           | 5.5               |
In power applications, an inductor often carries a DC current in addition to a high-frequency AC current. Therefore, it is important to also account for DC performance when evaluating the performance of the power MEMS inductor. Figure 11b shows the inductance density versus a figure of merit (FOM) for previous MEMS power inductors. We introduce the FOM to better scope the inductor efficiency at both DC and AC frequencies. The FOM is calculated using (1).

\[ FOM = \frac{\sqrt{Q_{DC} Q_{AC}}}{V} = \frac{L_{DC}}{R_{DC} Q_{\text{max}}/V} \]  

(1)

where \( Q_{DC} \) is the low-frequency quality factor, \( Q_{\text{max}} \) is the maximum quality factor, \( V \) is the total inductor volume, \( L_{DC} \) is the low-frequency inductance, and \( R_{DC} \) is the DC resistance. It is noted that the inductor substrate thickness is chosen to be 350 µm unless otherwise mentioned. It is shown in Fig. 11b that 3D in-Si toroidal inductors also outperform 2D on-Si toroidal inductors with higher inductance densities and FOMs, as shown in Fig. 11b. On the other hand, on-Si inductors cover a wider range of \( Q \) (3–19) and inductance density (25–110 nH/mm²).

While air-core MEMS inductors are useful for switching at very high frequencies (VHFs) above 22 MHz, magnetic-core MEMS inductors are needed for DC–DC power supplies below 22 MHz to achieve sufficient inductance. However, the advances in power conversion technologies have outpaced the growth in magnetics, and magnetic materials have become a key limitation constraining the overall miniaturization due to their excessive core losses at HF and VHF frequency ranges. Fundamental understandings of the core losses can be found in references 31,99.

Developments in magnetic technology for power MEMS inductors have focused on exploring novel material combinations, optimizing core structures, and developing integration technology for magnetic materials. Electroplated ferrites, such as Ni_{45}Fe_{55}^{100}, have been intensively studied due to their ease of fabrication, high permeability, and useful frequency range (MHz). Nano-granular cobalt-based alloys have recently received much attention due to their low core loss at high frequencies 26,101,102. Notable studies of MEMS inductors with this material category include CoNiFe 38, sputtered Co–Zr–O 26, Ta/Co_{93.5}Zr_{4.0}Ta_{4.5} (CZT)/SiO_{2} 101, and sputtered cobalt-based amorphous alloys 102. This approach often requires advanced deposition techniques for nanolaminated thin-film structures. Alternating electrodeposition and co-sputtering are the two most common deposition methods that have been demonstrated.

Another notable category of magnetic cores is composite cores. Using microscale and nanoscale magnetic particles that are electrically isolated, the eddy current loss can be significantly reduced, thus extending nano-composite materials to high-frequency applications. Magnetic composites consist of magnetic particles that are electrically isolated either by insulator shells or by non-conducting media such as polymers. Casting or screen printing has the advantage of forming a large-volume magnetic core at low costs.

Packaging technology for PwrSoC

For PwrSoC research, packaging technology plays a crucial role in improving the power density and efficiency for efficient thermal dissipation and minimal unwanted parasitics. For heat dissipation, high-thermal-conductivity materials such as Al_{2}O_{3} and AlN are used as substrates and encapsulation materials. MEMS packaging technologies are adopted for PwrSoC integration as an alternative for common packaging architectures such as leaded-frame power modules and PCB-embedded power modules. There are 2D/2.5D packaging architectures that use wire bonding 103 or flip-chip bonding techniques 104. On the other hand, 3D packaging architectures refer to the vertical stacking of ICs using TSV-based Si interposers. Vertical stacking using TSV interconnections reduces the electrical path, thus minimizing the parasitics between vertically stacked chips. In addition, TSV-based packaging technology provides efficient thermal dissipation due to spreading effects over a thermally conductive substrate 105, thus enhancing the power density and efficiency of PwrSoC. Important challenges are MEMS-CMOS integration of passive components such as inductors, TSV process optimization to maximize the current-carrying capability, and TSV insulator technology optimization to achieve CMOS compatibility and high-voltage isolation while keeping the TSV substrate thermal resistance low. Low-temperature ALD-enabled dielectrics, such as Al_{2}O_{3} and AlN, are promising alternatives for dielectrics deposited by PECVD. Table 3 summarizes the key specifications of the power converters shown in Fig. 10, including the converter efficiency and power density corresponding to 2D, 2.5D, and 3D packaging technologies.

Challenges and research opportunities for power electronics

Power supply technology needs to keep up with the rapid development pace of modern electronics with respect to size reduction and performance improvement. Integrated power supplies have the potential to become an ideal solution. However, to increase the integration level, we envision the further development of four aspects.

First, further developments are needed to optimize the winding design and magnetic materials. We believe that inductors constructed by using 3D windings and TSV windings have great potential for the MHz switching
Frequency. 3D solenoid and toroidal windings have been shown to have better performance in terms of the inductance density and power density. Although these winding structures have been intensively studied, accurate models of winding losses are still needed to minimize losses due to eddy-current effects, especially the proximity effect.

Second, magnetic materials and deposition technologies are essential for power MEMS inductors. In addition to the deposition methods studied intensively, such as electroplating and sputtering, atomic layer deposition (ALD) is an emerging deposition method for fabricating nanolaminated magnetic thin films. ALD provides unique advantages, depositing alternating thin-film systems with superior flexibility and controllability over the film thickness, quality, and uniformity. The challenge is the limited variety of available magnetic materials that can be deposited by ALD. Superparamagnetic particles could also be interesting to investigate due to their extremely...
neural activity. In 1985, Barker et al. demonstrated the use of TMS-based interposer technology is a promising approach towards 3D integration of the power supply. Several intermediate steps are to be carried out towards monolithically integrated PwrSoC, including passive interposers, active interposers, and active-passive interposers. Several integrated power supplies have been demonstrated using passive interposers, such as inductive interposers and capacitive interposers.

Finally, MEMS–CMOS integration is a crucial technology for PwrSoC integration. This technology would enable the monolithic integration of MEMS passive components (e.g., inductors and capacitors) and active components on the same substrate. A CMOS-compatible technology for a power MEMS inductor is needed.

Biomedical and neurotechnology applications

MEMS inductors and magnetic devices also find important applications in the field of biomedical devices and systems, including microfluidics (nanobead trapping, magnetic sensing, and biotarget sorting), nuclear magnetic resonance (NMR) spectroscopy, implantable biomedical devices, magnetic stimulation, and excitation (excitable cells and neurostimulation). There are review papers covering the first three application categories, such as microfluidics, magnetic sensing, NMR, wireless power transfer for implantable medical devices, and NMR technologies for biomedical applications. However, there is no review on the last application category. In this section, we focus on an exciting and growing area of microinductor research and application: neurotechnology.

Since the nervous system uses electrical signals to perform information transmission and to control the sensory organs, external electromagnetic fields can modulate neural activity. In 1985, Barker et al. demonstrated the stimulation of neurons using localized transcranial magnetic stimulation (TMS). Over the last 20 years, TMS, which uses rapidly fluctuating magnetic fields, has emerged as a noninvasive and painless technique to modulate brain function and brain mapping and to explore the excitability of different brain regions. Furthermore, TMS has been employed for the detection and monitoring of neurodegenerative diseases and for clinical therapy due to its ability to dampen neuronal hyperexcitability, decrease neuroinflammation, alter blood-brain-barrier permeability and promote neuronal survival.

The magnetic flux created due to dynamic current flow through the coil generates its own electric field. This electric field induces changes in transmembrane currents, eventually leading to the depolarization or hyperpolarization of neurons, making them, respectively, more or less excitable. Depending on the frequency, duration, and intensity of stimulation, the effects of TMS can be varied. Low-frequency and high-frequency stimulation patterns can, respectively, exert dampening of neural activity and excitatory effects on brain activity. Single-pulse and paired-pulse TMS are used to examine the functionality of the brain, whereas repetitive TMS is utilized to induce long-lasting changes in brain activity beyond the stimulation period, as summarized in Fig. 12a. Chronic prosthetic applications require deeper brain activation with accurate focusing of specific neural targets.

Micromagnetic stimulation (μMS)

μMS uses an implanted MEMS microcoil to produce a magnetic field. Unlike TMS, which uses a relatively large coil, e.g., often 50–100 mm in diameter, that is positioned above the scalp (Fig. 12a) and typically targets large regions in the superficial cortex (e.g., several centimeters or more in diameter), the use of MEMS allows coils to be implanted into the brain and may facilitate confined activation of narrow regions of the brain or even a single neuron. Bonmassar et al. reported, for the first time in 2012, that the electric currents flowing through the commercially available microcoil inductor generated adequate time-varying magnetic fields and, in the process, could induce electric currents in a focal area to elicit neuronal activity. This development raises new possibilities of using a micromagnetic stimulation inductor as neural prosthetics, which would allow implantation near the areas of interest to stimulate deeper brain targets with higher spatial selectivity. Figure 13 summarizes the timeline of development and the applications of non-invasive micromagnetic stimulation of brain activation.

For example, Lee et al. used a commercial solenoid coil (0.5 mm in diameter) to stimulate subthalamic nucleus (STN) neurons, i.e., the primary target of deep brain stimulation for the treatment of Parkinson’s disease. A similar approach was reported by Minusa et al., where microcoil magnetic stimulation using the same solenoid coil was employed for activation of the auditory cortex of anesthetized mice. The results show that μMS can selectively target local neural networks and modulate their activities in vivo. Unfortunately, because commercial microcoils are not designed for implantation into the cortex, tissue damage during implantation is a serious problem. Therefore, dedicated MEMS coil implants are needed.

In 2016, the first MEMS microcoil-based neural prosthetics were reported. The coil had a half turn because it was fabricated using the 2D lithography method. The width and length of the implant were 100 μm and 2 mm, respectively. The implant was tested in living mouse subjects. Despite generating a weaker electric field than...
that of large TMS coils, the field was confined to a much smaller region, and therefore, the spatial gradient of the field was strong enough to activate neurons in both in vitro and in vivo experiments. The implant was inserted into the mouse whisker motor cortex, and depending on the stimulation frequency, the whiskers exhibited movements in response to microcoil stimulation (Fig. 12b). Although this inductor is thin and small, there is still room for improvement in terms of its magnetic field strength and selectivity. A study showed that the coil design (e.g., shape and number of turns) influenced the selectivity and strength of the microcoil\textsuperscript{137}. Several microcoil designs, namely, rectangular, V-shaped and W-shaped designs, were studied numerically and experimentally in vitro using coronal brain slices from the mouse primary visual cortex. The results show that both the V-shaped and W-shaped designs can reliably activate neurons. The W-shaped coil design provides higher selectivity, whereas the V-shaped coil design renders a higher strength of stimulation. Moreover, when compared to the single-turn coil design, the multiturn coil exhibits enhanced strength of stimulation and thus reduces the activation thresholds. The findings present guidelines for the development of next-generation microcoil-based neural prostheses.

**Challenges and research opportunities for neurotechnologies**

Since its first manifestation in the mid-1980s, the TMS method has evolved to overcome some of the issues associated with electric brain stimulation\textsuperscript{138}, such as pain links to the stimulation process and tissue damage. However, the noninvasive nature of TMS limits its specificity and focality. This makes deeper brain area activation difficult without affecting greater regions than the targeted location. Since divergent magnetic stimulation could increase the risk of seizures and other side effects\textsuperscript{139}, design optimization of the appropriate coil has become increasingly important, and challenging to improve the focality for brain stimulation\textsuperscript{140}. The multichannel TMS approach\textsuperscript{141}, where multiple independent coils are simultaneously operated with altered magnitudes of current to produce a magnetic field profile in demand, has also been developed to overcome issues. Although the multichannel approach shows promise, the energy and thermal dissipation still need to be addressed. Another drawback of the TMS is variability, which contributes to uncertainty and inefficiency. Often, the results of the TMS are inconsistent. A study showed that a particular sequence of pulse patterns could produce different responses for different persons\textsuperscript{140}.

Progress in μMS employing microcoil implants allows for ultrafocused intracortical stimulation and focal cortical responses around coil implants. Compared to TMS, micromagnetic stimulation coils can be positioned in close proximity to the target region, which helps to improve the spatial control of the elicited activity. Additionally, compared to recently developed implantable neural stimulators powered by using inductive coupling coils\textsuperscript{142}, magnetic transducers\textsuperscript{143,144}, and ultrasound transducers\textsuperscript{145,146}, microcoil implants have important advantages. For example, regardless of the method of wireless power transmission, since most wireless stimulators generally deliver direct electric stimulation to targeted neurons via implanted electrodes, there are several limitations, such as limited control of the electric fields (e.g., spatially symmetric electric fields) and decreased performance associated with tissue inflammation (e.g., glial scarring). In contrast, microcoil implants can produce spatially asymmetric electric fields around the coils, thereby selectively targeting specific neurons while avoiding passing axons. This enhanced selectivity suggests that coil implants can provide better stimulation resolution than electrode-based implants. Additionally, since the magnetic field has high permeability to biological materials, the efficacy of magnetic stimulation from the coil implants will not be diminished even by severe tissue encapsulation. Thus, microcoil implants have the potential to improve the effectiveness and reliability of implantable neural stimulators.

Since magnetic fields can also pass through nonmagnetic insulating materials, microcoils can be fully encapsulated using a wide range of flexible biocompatible materials, e.g., Parylene\textsuperscript{147}, liquid crystal polymer\textsuperscript{148}, and hydrogel\textsuperscript{149}; this will help to reduce the inflammatory tissue reactions that can arise in response to chronic implantation in the cortex. This encapsulation also enables the μMS coils to be electrically isolated from the adjacent tissue and may also reduce the amount of heat transfer. However, regarding the mechanisms underlying μMS induction, e.g., modulation of the activity of single neurons or cortical neural networks, we have a very limited understanding\textsuperscript{150,151}.

For neural prosthetic implants with ultrafine stimulation resolution, we envision opportunities and challenges in four areas. First, since a 3D microcoil requires dimensions similar to those of neuron cells (20 µm), there are significant fabrication challenges in fabricating multiturn inductors with conductors approximately 1 µm in diameter and in performing magnetic core integration to achieve a high inductance density. Second, unlike the RF and power electronics applications, inductors for neural stimulations must induce large electrical field gradients with low power consumption. Hence, the inductor designs are very different and have only marginally been explored. Third, for medical applications in artificial vision, an array of millions of inductors is needed, and the array must be implanted in the visual cortex with a complex topology. The challenge is to make individualized, flexible, multiplexed, and durable implants. Fourth, since there are 30 million blind people...
around the world and most patients cannot afford expensive implants, the final challenge is to provide accessible technology.

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Conflict of interest

Dr. Le is a co-founder and holds an equity stake in Lotus-Microsystems APS, Denmark. Other authors do not have any conflicts of interest.

Supplementary information

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References

1. Hilmat, O. F. & Mohamed Ali, M. S. RF MEMS inductors and their applications — a review. J. Micromech. Microeng. 26, 17–44 (2017).
2. Li, X., Ni, Z., Gu, L., Wu, Z. & Yang, C. Micromachined high-performance RF passives in CMOS substrate. J. Micromech. Microeng. 26, 113001 (2016).
3. Ahn, C. H. & Allen, M. G. A fully integrated surface micromachined magnetic microactuator with a multilevel meander magnetic core. J. Micromech. Microeng. 2, 15–22 (1993).
4. Ahn, C. H. & Allen, M. G. Micromachined planar inductors on silicon wafers for MEMS applications. IEEE Trans. Ind. Electron. 45, 866–876 (1998).
5. Sullivan, C. R., Sullivan, C. R., S. & S. R. Design of microfabricated transformers and inductors for high-frequency power conversion. IEEE Trans. Power Electron. 11, 228–238 (1996).
6. Sato, T. et al. A magnetic thin film inductor and its application to a MHz switching dc-dc converter. IEEE Trans. Magn. 30, 217–223 (1994).
7. Lopez-Villejas, J. M., Martiner, J., Cane, C., Losantos, P. B. & Bausells, J. Improvement of the quality factor of RF integrated inductors by layout optimization. IEEE Trans. Magn. Theory Tech. 48, 76–83 (2002).
8. Patrick Yue, C. & Simon Wong, S. Physical modeling of spiral inductors on silicon. IEEE Trans. Electron Devices 47, 560–568 (2000).
9. Cao, Y. et al. Frequency-independent equivalent-circuit model for on-chip spiral inductors. IEEE J. Solid State Circuits 38, 419–426 (2003).

10. Anthony, R., Laforge, E., Casey, D. P., Rohan, J. F. & O'Mathuna, C. High-aspect-ratio photoresist processing for fabrication of high resolution and thick micro-windings. J. Micromech. Microeng. 26, 105012 (2016).
11. Brunet, M., O'Donnell, T., O'Brien, J., McCluskey, P. & Mathuna, S. C. O. Thick photoresist development for the fabrication of high aspect ratio magnetic coils. J. Micromech. Microeng. 12, 444–449 (2002).
12. Bourner, D., Ghannam, A., Dilhan, M. & Granier, H. Potential of BPN as a new negative photoresist for a very thick layer with high aspect ratio. Microsyst. Technol. 20, 2089–2096 (2014).
13. Xue, C., Yao, F., Cheng, B. & Wang, Q. Effect of the silicon substrate structure on spiral micro inductor. Front. Electron. Eng. China 3, 110–115 (2008).
14. Raeeszadegh, M., Monajemi, P., Yoon, S.-W., Lash-ar, J. & Ayazi, F. High-Q integrated inductors on trenched silicon islands in 18th IEEE International Conference on Micro Electro Mechanical Systems 199–202 (IEEE, 2005).
15. Raes-Zadeh, M. & Ayazi, F. Characterization of high-Q spiral inductors on thick silicon-on-silicon. J. Micromech. Microeng. 15, 2105–2112 (2005).

Tuntusya, E. G. & Webb, S. High performance MEMS inductors fabricated on localised and planar thick SiO2 layer. Electron. Lett. 41, 40–41 (2005).

17. Yang, M. Z., Dai, C. L. & Yang, H. Manufacture and characterization of high-Q factor inductors based on CMOS-MEMS techniques. Sensors 11, 9798–9806 (2011).

18. Sun, Y., van Zeijl, H., Tauritz, J. L. & Baets, R. G. F. Suspended membrane inductors and capacitors for application in silicon MEMS. IEEE 1996 Microwave and Millimeter-Wave Monolithic Circuits Symposium. Digest of Papers, 1996, pp. 99–102.

19. Yoon, J. B., Han, C. H., Yoon, E. & Kim, C. K. Monolithic high-Q overhang inductors fabricated on silicon and glass substrates, International Electron Devices Meeting 1999 Technical Digest (Cat. No.99CH36318), 1999, pp. 753–756.

20. Lakdawala, H. et al. Micromachined high-Q inductors in a 0.18-μm copper interconnect low-k dielectric CMOS process. IEEE J. Solid State Circuits 37, 394–403 (2002).

21. Zheng, T., Xu, G. & Luo, L. High performance suspended spiral inductor and band-pass filter by wafer level packaging technology. Microsyst. Technol. 23, 2107–2111 (2017).

22. Wang, G. et al. Novel on-chip spiral inductors with back hollow structure. Mod. Phys. Lett. B 31, 4–6 (2017).

23. Ding, Y., Fang, X., Wu, R., Guo, Q. & Sin, J. K. O. A suspended thindisk-type inductor for integrated voltage regulator applications. IEEE Electron Device Lett. 41, 95–98 (2020).

24. Tai, C. M. & Liao, C. N. Multilevel suspended thin-film inductors on silicon wafers. IEEE Trans. Electron Devices 54, 1510–1514 (2007).

25. Wang, X. N., Zhao, X. L., Zhou, Y., Dai, X. H. & Cai, B. Fabrication and performance of a novel suspended RF spiral inductor. IEEE Trans. Electron Devices 51, 814–816 (2004).

26. Harburg, D. V. et al. Microfabricated racetrack inductors with thin-film magnetic cores for on-chip power conversion. IEEE J. Emerg. Sel. Top. Power Electron. 6, 1280–1294 (2018).

27. Harburg, D. V. et al. Measured performance and micro-fabrication of racetrack power inductors, 2013 IEEE Energy Conversion Congress and Exposition, 2013, pp. 614–620.

28. Harburg, D. V. et al. Micro-fabricated thin-film inductors for on-chip power conversion in 2012 7th International Conference on Integrated Power Electronic Systems 2–7 (IEEE, 2012).

29. Wang, N. et al. High-frequency micro-machined power inductors. J. Magn. Magn. Mater. 290–291, 1347–1350 (2005).

30. Bellarej, M. F., Davis, A. K., Kohl, P. & Swaminathan, M. Magnetic core solenoid power inductors on organic substrate for system in package integrated high frequency voltage regulators. IEEE J. Emerg. Sel. Top. Power Electron. 30332, 1–1 (2019).

31. Mathuna, C. O., Wang, N., Kulikami, S. & Roy, S. Review of integrated magnetics for power supply on chip (PwrSoC). IEEE Trans. Power Electron. 27, 4799–4816 (2012).

32. Zia, M., Oh, H. & Bakir, M. S. Post-CMOS fabrication technology enabling simultaneous fabrication of 3-D solenoid micro-inductors and flexible I/Os. IEEE Trans Compon. Packag. Manuf. Technol. 8, 2039–2044 (2018).

33. Cayton, A., Vailion, C., Bushueva, O., Ghannam, A. & Parra, T. High performance compact 3-D solenoids for RF applications. IEEE Micro. Wirel. Compon. Lett. 28, 479–481 (2018).

34. Gu, L. & Li X. High-Q solenoid inductors with a CMOS-compatible concave-suspending MEMS process. J. Micromech. Microeng. 16, 1162–1172 (2007).

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141. Minusa, S., Muramatsu, S., Osanai, H. & Tatero, T. A multichannel magnetic stimulation system using submillimeter-sized coils: system development and experimental application to rodent brain in vivo. J. Neural Eng. 16, 066014 (2019).

142. Freeman, D. K. et al. A sub-millimeter, inductively powered neural stimulator. Front. Neurosci. 11, 1–12 (2017).

143. O’Handley, R. C., Huang, J. K., Bono, D. C. & Simon, J. Improved wireless, transcutaneous power transmission for in vivo applications. IEEE Sens. J. 8, 57–62 (2008).

144. Rupp, T., Truong, B. D., Williams, S. & Roundy, S. Magnetoelctric transducer designs for use as wireless power receivers in wearable and implantable applications. Materials 12, 512 (2019).

145. Seo, D. et al. Wireless recording in the peripheral nervous system with ultrasonic neural dust. Neuron 91, 529–539 (2016).

146. Neely, R. M., Parch, D. K., Santa Cruz, S. R., Mahabirz, M. M. & Carmen, J. M. Recent advances in neural dust: towards a neural interface platform. Curr. Opin. Neurobio. 50, 64–78 (2018).

147. Kuppasimi, S. & Osłocie, R. H. Parylene coatings in medical devices and implants: a review. J. Biomed. Mater. Res., Part B 93B, 9–14 (2015).

148. Ahn, S. H., Jeong, J. & Kim, S. J. Emerging encapsulation technologies for long-term reliability of microfabricated implantable devices. Microchimica Acta 10, 1–22 (2019).

149. Madhusudanan, P., Raju, G. & Shankarappa, S. Hydrogel systems and their role in neural tissue engineering. J. R. Soc. Interface 17, 20190505 (2020).

150. Ryu, S. B. et al. Spatially confined responses of mouse visual cortex to intracranial magnetic stimulation from micro-coils. J. Neural Eng. 17, 056036 (2020).

151. Lee, S. W. & Fried, S. I. Enhanced adhesion in two-photon polymerization direct laser writing. AP Adv. 10, 045217 (2020).

152. He, S. et al. Facile fabrication of true three-dimensional micromirrors inside fused silica by a femtosecond laser. J. Microelectromech. Syst. 22, 105017 (2012).

153. Huang, W. et al. Three-dimensional radio-frequency transformers based on a self-rolled-up membrane platform. Nat. Electron 1, 305–313 (2018).

154. Izard, A. G. et al. Enhanced encapsulation technologies for high-frequency passives interposer. Micron 147, 267–296 (2021).

155. Anthon, R., Wang, N., Casey, D. P., Mathúna, C. & Rohan, J. F. MEMS fabrication of high-frequency integrated inductors on Ni-Cu-Zn ferrite sub- strates. J. Magn. Magn. Mater. 406, 89–94 (2016).

156. Yoon, Y. K., Park, J. W. & Allen, M. G. A sacrificial layer approach to highly laminated magnetic cores. Technical Digest - MEMS 2002: IEEE International Conference. Fifteenth IEEE International Conference on Micro Electro Mechanical Systems (Cat. No.02CH37266), 2002, pp. 380–383.

157. Anthony, R., Wiang, N., Casey, D. P., Mathúna, C. & Rohan, J. F. MEMS based fabrication of high-frequency integrated inductors on Ni-Cu-Zn ferrite substrate. J. Magn. Magn. Mater. 406, 89–94 (2016).

158. Yoon, Y. K., Park, J. W. & Allen, M. G. Polymer-core conductor approaches for RF MEMS. J. Micromech. Microeng. 14, 886–894 (2004).

159. Yu, X. et al. Silicon-embedding approaches to 3-D toroidal inductor fabrica- tion. J. Micromech. Microeng. 22, 580–588 (2013).

160. Fang, X., Wu, R., Peng, L. & Sin, J. K. O. A novel integrated power inductor with vertical laminated core for improved L/R ratios. IEEE Electron Device Lett. 35, 1287–1289 (2014).

161. Kim, J., Kim, K. J., Kim, M., Herrault, F. & Allen, M. G. Microfabrication of toroidal inductors integrated with nanolaminated ferrimagnetic metallic cores. J. Micromech. Microeng. 33, 114006 (2013).

162. Qu, J., Harburg, D. V. & Sullivan, C. A. Toroidal power inductor using radial-anisotropy thin-film magnetic material based on a hybrid fabrication process, 2013 Twenty-Eighth Annual IEEE Applied Power Electronics Conference and Exposition (APEC), 2013, pp. 1660–1667.

163. Wu, R., Liao, N. & Fang, X. A novel double-side silicon-embedded in. IEEE Transaction on Electron Devices 1–4 (IEEE, 2016).

164. Li, H. Y. et al. Three-dimensional solenoids realized via high-density deep coil stacking for MEMS application. IEEE Electron Device Lett. 33, 432–434 (2012).

165. Sun, T. et al. Substrate-embedded low-resistance solenoid inductors for integrated voltage regulators. IEEE Trans. Compon. Packag. Manuf. Technol. 10, 134–141 (2020).

166. Bleiker, S. J. et al. High-aspect-ratio through silicon vias for high-frequency application fabricated by gold-coated nickel wires. IEEE Trans. Compon. Packag. Manuf. Technol. 5, 21–27 (2015).

167. Li, H. et al. Fabrication and optimization of high aspect ratio through-silicon vias electroplating for 3D inductor. Microchimica Acta 9, 528 (2018).

168. Zhang, W., Gu, J., Xu, G., Luo, L. & Li, X. An optimized through-via bottom-up method for simultaneous-filling TSVs of different aspect-ratios and its potential application on high-frequency passive interposer. Microelectron. J. 101, 104798 (2020).

169. Tao, Z. et al. A radial-flux permanent magnet micromotor with 3D solenoid iron-core MEMS in-chip coils of high aspect ratio. IEEE Electron Device Lett. 41, 1090–1093 (2020).

170. Qu, C., Zhu, Z., En, Y., Wang, L. & Liu, X. Area-efficient extended 3-D inductor based on TSV technology for RF applications. IEEE Trans. Large Scale Integr. Systems 29, 267–296 (2021).

171. He, S. et al. High-aspect-ratio through-silicon vias electroplating for 3D inductor. IEEE Trans. Electron Devices 50, 718–729 (2003).

172. Van Dop, W. F., Van Someren, B., Hagen, C. W., Kruit, P. & Crozier, P. A. Approaching the resolution limit of nanometer-scale electron beam-induced deposition. Nano Lett. 5, 1303–1307 (2005).

173. Nakazawa, H. et al. Micro-DC-DC converter that integrates planar inductor on power IC. IEEE Trans. Magn. 36, 3518–3520 (2000).

174. Jia, H., Lu, J., Wang, X., Padmanabhan, K. & Shen, Z. J. Integration of a monolithic buck converter power IC and bondwire inductors with ferite epoxy glob cores. IEEE Trans. Power Electron. 26, 1627–1630 (2011).

175. Wang, N. et al. High frequency DC-DC converter with co-packaged planar inductor and power IC. 2013 IEEE 63rd Electronic Components and Technology Conference, 2013, pp. 1946–1952.

176. Fang, X. et al. A low substrate loss, monolithically integrated power inductor for compact LED drivers. In Proceedings of International Symposium on Power Semiconductor Devices ICs 53–56 (IEEE, 2015).

177. Lee, M., Choi, Y. & Kim, J. A 500-MHz, 0.76-W/mm² power density and 76.2% power efficiency, fully integrated digital buck converter in 65-nm CMOS. IEEE Trans. Ind. Appl. 52, 3315–3323 (2016).

178. Li, J., Tseng, V. F. G., Xiao, Z. & Xie, H. A high-Q in-silicon power inductor designed for waffer-level integration of compact DC-DC converters. IEEE Trans. Power Electron. 32, 3858–3867 (2017).

179. Ding, Y. et al. A power inductor integration technology using a silicon interposer for DC-DC converter applications. In Proceedings of International Symposium on Power Semiconductor Devices ICs 347–350 (IEEE, 2018).

180. Renz, P., Kaufmann, M., Lueders, M. & Wilch, B. A fully integrated 85%-peak-efficiency hybrid multi-ratio resonant DC-DC converter with 3.0-to-4.5V input and 300 µA-to-120 mA load range. In 2019 IEEE International Solid-State Circuits Conference (ISSCC), 156–158 (IEEE, 2019).

181. Liu, H. T. et al. Microfabricated air-core toroidal inductor in very high-frequency power converters. IEEE J. Emerg. Sel. Top. Power Electron. 6, 604–613 (2018).

182. Tischler, H. et al. Mini-coil for magnetic stimulation in the behaving primate. J. Neurosci. Methods 194, 242–251 (2011).