An effective detachment system for human induced pluripotent stem cells cultured on multilayered cultivation substrates using resonance vibrations

Yusuke Terao1,6, Yuta Kurashina2,3,6, Shugo Tohyama4,5,6, Yuki Fukuma3, Keiichi Fukuda4, Jun Fujita4* & Kenjiro Takemura2*

Clinical application of human induced pluripotent stem cells (hiPSCs) has been hampered by the lack of a practical, scalable culture system. Stacked culture plates (SCPs) have recently attracted attention. However, final cell yields depend on the efficiency of cell detachment, and inefficient cell recovery from SCPs presents a major challenge to their use. We have developed an effective detachment method using resonance vibrations (RVs) of substrates with sweeping driving frequency. By exciting RVs that have 1–3 antinodes with ultra-low-density enzyme spread on each substrate of SCPs, 87.8% of hiPSCs were successfully detached from a 5-layer SCP compared to 30.8% detached by the conventional enzymatic method. hiPSC viability was similar after either method. Moreover, hiPSCs detached by the RV method maintained their undifferentiated state. Additionally, hiPSCs after long-term culture (10 passages) kept excellent detachment efficiency, had the normal karyotypes, and maintained the undifferentiated state and pluripotency. These results indicated that the RV method has definite advantages over the conventional enzymatic method in the scalable culture of hiPSCs using SCPs.

Human induced pluripotent stem cells (hiPSCs) have the potential to differentiate into any type of cell, and can be used for disease modeling and drug discovery. They have also shown promise as a cell source for regenerative therapies1–3. In 2014, hiPSC-derived retinal pigment epithelial cell sheets were generated for treatment of age-related macular degeneration, and the cells were successfully transplanted for the first time by Takahashi et al.5. However, the number of transplanted cells was relatively small (graft size: 1.3 × 3 mm², cell density: 4,500 < viable cells/mm² < 29,000). On the basis of the success of the first clinical trial, hiPSCs have also received broad attention in regenerative therapies for much larger organs, such as the heart, liver, and spine6–8. Notably, heart regenerative therapies require a large number of cultured cells, because the heart consists of 1 × 10⁹–10¹⁰ cardiomyocytes9. To prepare such a large number of high-quality cardiomyocytes, many hiPSCs capable of cardiac differentiation are required, because terminally differentiated cardiomyocytes lose their proliferation ability10.

Several scalable hiPSC culture techniques have been investigated11, but highly efficient and stable mass culture is still in the trial phase for clinical study. Three-dimensional (3D) suspension culture, 3D sphere culture12, microcarrier suspension culture13,14, and spinner and bioreactor culture methods15–17 have been researched. On the other hand, even though 2D culture systems have several advantages for hiPSC culture, especially in the

1School of Science for Open and Environmental Systems, Graduate School of Science and Technology, Keio University, 3-14-1 Hiyoshi, Kohoku-ku, Yokohama, 223-8522, Japan. 2Department of Mechanical Engineering, Faculty of Science and Technology, Keio University, 3-14-1 Hiyoshi, Kohoku-ku, Yokohama, 223-8522, Japan. 3Department of Materials Science and Engineering, School of Materials and Chemical Technology, Tokyo Institute of Technology, 4259 Nagatsutacho, Midori-ku, Yokohama, 226-8503, Japan. 4Department of Cardiology, Keio University School of Medicine, 35 Shinanomachi, Shinjuku-ku, Tokyo, 160-8582, Japan. 5Department of Organ Fabrication, Keio University School of Medicine, 35 Shinanomachi, Shinjuku-ku, Tokyo, 160-8582, Japan. 6These authors contributed equally: Yusuke Terao, Yuta Kurashina and Shugo Tohyama. *email: jfujita@keio.jp; takemura@mech.keio.ac.jp
maintenance of pluripotency and quality control, they are thought inappropriate for mass culture, because the limited culture surface restricts maximum cell numbers and demands intensive labor.

As for an efficient method for cell detachment, we detached cells from small-scale cell culture dishes using resonance vibration (RV). Employing RV of dishes enables us to effectively obtain cells without damage compared to enzyme detachment methods. As for the long-term culture, the automated 2D hiPSCs culture system on the dish was developed and the obtained hiPSCs had a potency of differentiation into three germ layer cells. The dexterous motion of robot arms mimicking manual procedures makes it possible to automate the culture process. The massive scale culture system must be invented to apply cell therapies to large organs, as well. 10^8–10^9 cells (30–300 ø60 culture dishes) are required, for instance, for the heart regeneration medicine. To overcome the drawbacks of 2D culture systems, we established a mass-2D culture system for hiPSCs using stacked culture plates (SCPs) and active gas ventilation.

Although these scalable culture systems enable large-scale cultivation of hiPSCs, both 3D and 2D culture systems require efficient cell recovery ratios to be useful. However, SCPs were not originally designed for recovery of adhesive cells, but for collection of supernatants to obtain vaccines and antibodies; thus, the process of detaching cells from SCPs is challenging. The chief difficulties are the limited mechanical stimulus provided by manual tapping in the detachment process and inefficient enzymatic activity. The total weight of a 10-layer SCP including culture medium is approximately 2 kg. Due to such a heavy weight, cell detachment efficiency highly depends on manual technique. Moreover, it is difficult to evenly spread the detaching solutions in all layers of multilayer systems.

To improve the cell collection ratio, mechanical stimuli should be applied equally and efficiently to all layers of the SCP system. In this study, we propose a new, efficient, and safe method of detaching large numbers of hiPSCs from all layers of an SCP system using RVs, which will contribute to the clinical and industrial application of hiPSCs. That is, we are able to apply sufficient stimulus to cells with a small excitation force, and detach cells efficiently by using RVs on the SCPs.

**Results**

**Cell detachment system and vibration characteristics.** The cell detachment system developed in this study is schematically illustrated in Fig. 1. Cells are cultured on each substrate layer of an SCP (Fig. 1a) and are subjected to a trypsin solution and RVs induced in each substrate layer by a vibrator (Fig. 1b); this combination of trypsin and vibration detaches the cells (Fig. 1c). The system as shown in Fig. 1d is composed of an SCP, a vibration generator and a jig used to fix the SCP onto the vibration generator. The SCP is mounted on the aluminum and fixed by bolts as shown in Fig. 1e. Rubber discs are placed in between the bolts and SCP.

![Image](image-url)
To accurately apply vibration stimuli to the cells on each substrate, the first to third out-of-plane RVs of each substrate of a single-layer SCP (Fig. S1) and 5-layer SCP (Fig. 2) were excited. The resonance frequency for each vibration mode was confirmed in advance by eigenvalue analysis using finite element analysis software (COMSOL Multiphysics 5.2, COMSOL Inc., Burlington, MA, USA). As shown in Fig. 2d–f, the resonance frequency ranges between 95.4 and 114.4 Hz. Consequently, the exciting frequency was swept between 50 Hz and 300 Hz over 30 s to apply vibration stimuli to the cells.

The vibration characteristics of the SCP were evaluated. Figure 2g shows vibration amplitudes at the center of the cultivation layer and the jig and (h) relative amplitude, $A_r$. The distributions of vibration amplitude are measured along the longer central axis of each cultivation layer with an input frequency corresponding to each resonance frequency of (i) the first out-of-plane resonant mode and (j) third out-of-plane resonant mode listed in Table SI. These amplitudes are normalized to their maximum values.

Figure 2. Three-dimensional (3D) CAD model of a 5-layer SCP used for eigenvalue analysis, results of eigenvalue analysis, and measurement by laser Doppler velocimetry. (a) 3D CAD model, (b) 3D mesh model using tetrahedral elements; (c) side planes colored purple are fixed for eigenvalue analysis. (d) The eigenvalue analysis of first out-of-plane resonant mode of SCP. Resonance frequency ranges between 95.4 and 114.4 Hz. (e) The eigenvalue analysis of second out-of-plane resonant mode of SCP Resonance frequency ranges between 148.0 and 166.6 Hz. (f) The eigenvalue analysis of third out-of-plane resonant mode of SCP Resonance frequency ranges between 234.5 and 256.4 Hz. (g) Vibration amplitude at the center of the cultivation layer and the jig and (h) relative amplitude, $A_r$. (i) The distributions of vibration amplitude are measured along the longer central axis of each cultivation layer with an input frequency corresponding to each resonance frequency of (i) the first out-of-plane resonant mode and (j) third out-of-plane resonant mode listed in Table SI. These amplitudes are normalized to their maximum values.
The number of collected, $N_\text{col}$, and remaining, $N_\text{rem}$, after each method. (b) The percentage of dead cells ($N_\text{de} / N_\text{col}$) obtained by dividing the number of dead cells, $N_\text{de}$, by the number of collected cells, $N_\text{col}$. (c) The number of cells obtained by resedeeing cells detached by the RV and CE methods into 60 mm dishes followed by culture for 72 h. The number of resedeeed cells, $N_\text{res}$, was $8.0 \times 10^4$. (d,e) Experiments employing 5-layer SCPs. The number of seeded cells is $1.75 \times 10^7$ (mean $\pm$ SD, $n = 4$). Cells were cultured for 4 days, then collected by the RV and CE methods. Vibration was excited for 1 min after trypsin treatment for 2 min and measured the number of cells by hemocytometer. The sweep frequency range was from 50 to 250 Hz and sweep cycle was 30 s. (d) The number of cells collected, $N_\text{col}$, and remaining, $N_\text{rem}$, after each method. (e) The percentage of dead cells ($N_\text{de} / N_\text{col}$) obtained by dividing the number of dead cells, $N_\text{de}$, by the number of collected cells, $N_\text{col}$.

**Cell detachment experiments with mouse myoblast cells.** To examine the efficacy of the proposed cell detachment method using RVs, we evaluated the number of live/dead cells, viability, and proliferation after detachment using the mouse myoblast cell line C2C12 (Riken Bio Resource Center, Ibaraki, Japan). We chose myoblasts because they are typical cells studied in tissue engineering and regenerative medicine, such as in regeneration models of skeletal muscle tissue and myoblast sheets for improving cardiac function. The appropriate sweep frequency and trypsinization time are defined in the Experimental Procedures. Figure 3a–c show the results of the experiment employing a single-layer SCP, and Fig. 3d,e show the results employing a 5-layer SCP. Cells were cultured for 4 days in advance and collected by the RV method. As a control, a technician collected cells with a typical trypsinization and hand taps (denoted the conventional method). Figure 3a shows the number of cells collected, $N_\text{col}$, and remaining, $N_\text{rem}$, after each method. Overall, 88.8% and 71.1% of the total cells ($N_\text{col} + N_\text{rem}$) were detached ($p < 0.05$, Student’s t-test) by the RV and the conventional enzymatic (CE) methods, respectively. Figure 3b shows the percentage of dead cells, $N_\text{de}$, divided by $N_\text{col}$. With each method, 3.6% and 3.9% of $N_\text{col}$ were dead. To evaluate proliferation ability after detachment, cells ($N_\text{col}$) detached by the RV and the CE methods were reseded into 60 mm dishes, cultured for 72 h, and counted (Fig. 3c). $N_\text{col}$ values after the RV and the CE methods were $10.7 \times 10^4$ and $9.3 \times 10^4$, respectively. Figure 3d shows the number of cells collected, $N_\text{col}$, and remaining, $N_\text{rem}$, by each method from a 5-layer SCP. As shown, 98.4% and 87.2% of the cells were detached ($p < 0.01$, Student’s t-test) by the RV and the CE methods, respectively. Figure 3e shows the percentage of dead cells, $N_\text{de}$, divided by $N_\text{col}$, and 7.6% and 9.3% of $N_\text{col}$ were dead after collection by the RV and CE methods, respectively.

**Cell detachment experiments with hiPSCs.** To validate the efficacy of the RV method for culturing PSCs, we conducted a similar experiment using hiPSCs (253G4; Kyoto University, Kyoto, Japan). We chose hiPSCs because they are typical stem cells that can be applied in tissue engineering and regenerative medicine,

![Diagram](https://example.com/diagram.png)
After detachment, we evaluated the representative immunofluorescence staining for NANOG, OCT4, TRA1-60, SSEA4, and nuclei in hiPSC-derived dispersed cells to validate the undifferentiated state of the cells collected with the RV method. Figure 4 shows the results of the experiments employing a 5-layer SCP. Figure 4a shows the number of cells collected, \( N_{ic5} \), and remaining, \( N_{ir5} \), by each method. Overall, 87.8% and 30.8% of the total cells (\( N_{ic5} + N_{ir5} \)) were detached (\( p < 0.01 \), Student’s t-test) by the RV and CE methods, respectively. Figure 4b shows the percentage of dead cells, \( N_{id5} / N_{ic5} \), obtained by dividing number of dead cells, \( N_{id5} \), by the number of collected cells, \( N_{ic5} \). (c,d) Representative immunofluorescence staining for NANOG (red), OCT4 (green), TRA1-60 (green), SSEA4 (red), and nuclei (blue) in hiPSC-derived dispersed cells detached by (c) the RV and (d) the CE methods. Scale bars represent 200 \( \mu \)m (NANOG and OCT4) and 100 \( \mu \)m (TRA1-60 and SSEA4).

Cell detachment during 10 passages with hiPSCs. In order to evaluate the safety of hiPSCs using our method, we show the growth curve during 10 passages, karyotypes, representative immunofluorescence staining and differentiation state after 10 passages. The total number of cells detached by RV is greater than those detached by CE from the results of the growth curve during 10 passages as shown in Fig. 5a. Hence, the result indicates that the growth curve of RV method increased greatly compared to that of the CE method as the number of passages increased. To confirm the safety of the chromosomes after repeated passages with RV, the karyotypes were observed (Fig. 5b). The karyotypes of the cultured hiPSCs was normal. In order to evaluate the undifferentiation state and pluripotency of the passaged cells, immunofluorescence staining and the flow cytometry analysis (FCA) were performed. Immunofluorescence staining confirmed strong expression of pluripotency markers in all colonies (Supplementary Fig. 3a,b). The FCA confirmed that following this metabolic selection, almost all cells (>99.5%) clearly expressed SSEA4 and TRA-1-60 (Fig. 5c,d). These data strongly indicated that the cells passaged by the RV method remained undifferentiated. Additionally, ectoderm, mesoderm, and endoderm differentiated from hiPSCs passaged by RV method were shown in Fig. 5e for the maintenance of pluripotency in hiPSCs.
Figure 5. Long term culture of 10 passages with hiPSCs using resonance vibrations. (a,b) The optimal vibration extension system for long term culture. Whole composition of the vibration excitation system (a), and installation of the SCPs mounted on the vibration system on the ground (b). (c) The results of the growth curve during 10 passages collected by the resonance vibration (RV) method and the conventional enzymatic (CE) method. (d) The karyotypes of the cultured hiPSCs were observed. (e,f) Representative flow cytometry analysis (FCA) for SSEA4 and TRA1-60 positive cells passaged by (e) the RV method and (f) the CE method. Photographs (a,b) permission acquired from SHIBUYA Corporation.
Discussion

After evaluating the vibration characteristics of the developed cell detachment system, we conducted detachment experiments with the mouse myoblast cell line C2C12 on single-layer and 5-layer SCPs to evaluate detachment efficiency, viability, and proliferation of the detached cells. Our results indicate that cells were detached more effectively by the RV method mediated by RVs of substrates than by the CE method of trypsinization. Additionally, viability and proliferation of the detached cells were similar after both detachment methods. Moreover, we conducted similar experiments using hiPSCs and validated the undifferentiated state of the detached cells by representative immunofluorescence staining analyses. The results indicate that the RV method is applicable to SCPs and maintains cell viability and the undifferentiated state.

The resonance frequencies of the employed vibration modes of each layer of an SCP are different, as shown in Table S1 and Fig. 2d–f. This difference is mainly caused by the constraint conditions of each layer. The bottom layer, for example, has four layers above it and is fixed to the jig around its circumference. On the other hand, the top layer has four layers below it. Owing to this difference in resonance, swept frequencies are required to excite the first, second, and third RVs on all layers. In this way, we can excite multiple RV modes of each layer, resulting in the application of mechanical stimuli to a wide area of each layer. That is, we can eliminate the presence of a vibration node from each resonance mode. In addition, sweeping the driving frequency has the advantage of exciting resonance vibrations with certainty. Generally, the resonance frequency of any elastic body is unstable depending on the, constraint conditions, and temperature, among other things. In the case of an SCP, its resonance frequency may depend on the volume of inner solution, surrounding temperature, and fixing conditions. Sweeping the input frequency overcomes this instability of resonance frequency and makes the RV method robust.

Equations S4 and S6 in the SI prove that the force applied to the cells is 10–1000 times higher during detachment by the RV method than that applied by the CE method. Moreover, in the CE method, the force is only applied once and briefly by a single tap. On the other hand, in the RV method, the force is continuously applied during excitation of the vibrations. The above estimation of the force applied to the cells suggests that the cell detaching efficiency can be improved with the RV method due to the significant improvement of the force applied to the cells.

In the detachment process, we used the enzymes trypsin-EDTA for C2C12 and TrypLE Select for hiPSCs. These proteinases may damage cell surfaces37,29; therefore, enzyme concentration and treatment duration are important factors, because the opportunity for the enzyme to break down cell surface proteins increases with both29,30. For this reason, the enzymes were diluted to 0.0125% trypsin-EDTA and 50% TrypLE Select, which are half the typical concentrations, and the durations of treatment were defined as 3 min and 5 min, which are the minimum times required for general immersion. The experimental results using the 5-layer SCP indicate that the percentage of total cells collected was approximately 90% after collection by the RV method, improving more than 10% and 50% for C2C12 cells and hiPSCs, respectively, compared with the percentage collected by the CE method, as shown in Figs 3d and 4a. This demonstrates the remarkable effectiveness of the RV cell detachment method.

The differences between the detachment ratios of C2C12 cells and hiPSCs may be due to differences in the protein degradation ability of trypsin-EDTA and TrypLE Select. Regardless, the RV method improves the detachment efficiency of both C2C12 cells and hiPSCs. This improvement will be more marked in larger-scale cell cultivation. The RV method also showed excellent detachment efficiency even during long-term culture (10 passages). In addition, hiPSCs after 10 passages had normal karyotypes and still maintained an undifferentiated state and pluripotency. Thus, the safety of the RV method was confirmed. In the case of heart regenerative therapy, the number of cells required is on the order of 10⁹ per person. Considering this, the RV method will greatly aid the mass culture required for such therapies. Furthermore, its improvements in culture efficiency will have great impact in the repetitive process of subculture.

In the future, as tissue engineering and regenerative medicine using autologous cultured cells develops, the time required to culture the necessary numbers of cells will become more and more important. In such an era of cell therapy, the RV cell detachment method will be an essential technique for mass cultivation in large vessels with multilayered substrates. Furthermore, this method can easily be applied in automated cell culture systems using 2D culturing, since the method requires no human hands.

Methods

Measurement of vibration characteristics. The vibration characteristics of SCP (CellStack® Culture Chamber; Corning, NY, USA) were measured using a laser Doppler vibrometer (LV-188; Ono Sokki, Yokohama, Japan) with an input voltage to the vibration generator (F-60K/60, EMIC Corporation, Tokyo, Japan) of 35 Vp-p. The amplitude of vibration velocity, \( A_v \), was measured at the centers of cultivation layers and at the jig, and then converted to vibration amplitude, \( A \), by

\[
A = \frac{A_v}{2\pi f}.
\]  

Additionally, the relative amplitude of substrate against that of the jig was calculated. Note that the input power is constant at the vibration generator, i.e., the amplitude of the vibration generator decreases as frequency increases. The resonance frequency was identified from the relative amplitude, \( A_r \), calculated as,

\[
A_r = \frac{A_i}{A_j},
\]  

where, \( A_i \) is the amplitude of the target layer of SCP, and \( A_j \) is the amplitude of the jig fixed to the vibration generator. When measuring amplitude distribution, vibration amplitudes were measured along the longer central axis of the cultivation layers. The input voltage to the vibration generator was set to 35 Vp-p and the driven frequency was adjusted to each resonance. Furthermore, the relative amplitude at each point was normalized by the maximum value.
Cell preparation. C2C12 mouse myoblast cells (RCB0987; Riken Bio Resource Center, Ibaraki, Japan), and hiPSCs (253G4; Kyoto University, Kyoto, Japan) were employed to evaluate the proposed RV method. The myoblasts were cultured in growth medium (D-MEM/F12 supplemented with 10% fetal bovine serum (FBS)), and hiPSCs were cultured in modified StemFit Medium. Both were cultured in a 5% CO₂ humidified atmosphere incubator at 37°C. Cell passage was performed by trypsinization in 0.050% trypsin-EDTA (25300; Invitrogen, Carlsbad, CA, USA) for myoblasts and TryPLE Select (1X) (Thermo Fisher Scientific, Waltham, MA, USA) for hiPSCs with pipetting.

Both cell types were passaged the minimum number of times needed for proliferation and were seeded in SCPs. In the experiments employing myoblasts, 3.5 × 10⁶ cells in 100 mL growth medium were seeded into each chamber of an SCP, i.e., 3.5 × 10⁶ cells in 100 mL and 1.75 × 10⁷ cells in 500 mL were seeded into single-layer and 5-layer SCPs, respectively. In the case of hiPSCs, we seeded 4 × 10⁶ cells into a 5-layer SCP coated with Matrigel (BD Biosciences, Franklin Lakes, NJ, USA). Cells at passage 4 were seeded with 100 mL growth medium into a 5-layer SCP coated with Matrigel. Both cell types were incubated for 4 days in a 5% CO₂ humidified atmosphere incubator at 37°C. The medium was exchanged 2 days after seeding. The cells were used as an initial sample in the following cell detachment experiments.

Cell detachment methods. To prove that the RV method is effective in detaching cells from the cultivation substrates of SCPs, we detached cells using both trypsinization with resonance vibrations in the RV method and trypsinization with manual tapping in the CE method.

In both methods, cells attached to the cultivation substrates were washed twice with phosphate-buffered saline (PBS), and then PBS (50 mL in each chamber) was spread into the chamber. Myoblasts and hiPSCs were detached from the substrate by the following step:

1. RV method: 0.0125% trypsin-EDTA for myoblasts or 50% TryPLE Select (1X) for hiPSCs was spread into the SCP (30 mL in each layer). After 2 min, the RVs were excited for 1 min in the case of myoblasts, i.e., the total duration of treatment was 3 min. For the hiPSCs, after 2 min, the resonance vibrations were excited for 1 min, and the SCP was allowed to rest for 2 min, i.e., the total duration of treatment was 5 min.

2. CE method: 0.0125% trypsin-EDTA for myoblasts or 50% TryPLE Select (1X) for hiPSCs was spread onto the SCP (30 mL in each layer). After 2 min, manual tapping was applied 3 times on each side of the SCP for 1 min in the case of myoblasts, i.e., the total duration of treatment was 3 min. In the case of hiPSCs, after 2 min, manual tapping was applied 3 times on each side of the SCP for 1 min, and the SCP was allowed to rest for 2 min, i.e., the total duration of treatment was 5 min. In order to reduce human error/intention, the technicians, who routinely culture hiPS cells using SCP22 and do not know the purpose of the research, carried out the experiments.

Note that, we used the half diluted trypsin-EDTA and TryPLE Select compared to standard concentration. This is because that trypsin-EDTA at a high concentration is known to damage cells23 and TryPLE Select is recommended to be diluted half in the protocol of the Center for iPS Cell Research and Application (CiRA) at Kyoto University. After the detachment process, medium was spread onto the SCP (15 mL in each layer) to neutralize trypsin. Cells were collected from the cultivation chamber by pipetting. In this procedure, to completely collect the detached cells, each cultivation substrate was washed with PBS (30 mL per layer) twice. In addition, the sweep frequency ranges of the AC input to the vibration generator were 50–250 Hz for a single-layer SCP and 50–300 Hz for a 5-layer SCP, which covered the range of resonance frequency up to the third out-of-plane resonance. The input voltage was set to 35 Vₚ−ₚ.

Counting of detached cells. The number of collected cells was counted using a hemocytometer (A116; Asone, Osaka, Japan) under a phase contrast microscopy (ECLIPSE Ti; Nikon Corporation, Tokyo, Japan), and this process was repeated 4 times. From this result, the ratio of detached cells to total cells (collected cells plus remaining cells) was calculated. Additionally, the ratio of cell survival was measured with the Trypan blue (Trypan Blue Solution (0.4%); Thermo Fisher Scientific) exclusion test on a hemocytometer, because cells may have died during the detachment process.

Counting of remaining cells. After detachment, the cells remaining in the SCP were removed from the cultivation substrates using thick trypsin-EDTA for a prolonged time and counted. That is, the cells were soaked in 0.025% trypsin-EDTA (15 mL in each layer) for 10 min at 37°C, and then collected by pipetting. In addition, to completely collect the cells, the cultivation substrates were washed with PBS (30 mL in each layer) twice, and cells were collected in PBS.

Cell proliferation assay. The cell proliferation ratio after the detachment process was evaluated by counting cell numbers after culture for a certain period of time. In particular, the myoblasts (8.0 × 10⁴ cells) detached with the RV and the CE methods were independently reseeded in 60 mm dishes (AGC Techno Glass Co., Ltd., Shizuoka, Japan) and incubated for 72 h. Afterwards, the number of cells was counted using a hemocytometer, and the cell counting was repeated 4 times.

Immunofluorescence staining. To confirm the pluripotency of hiPSCs, the cells were immunostained with pluripotency markers. Cells were washed with PBS and fixed with 4% paraformaldehyde for 20 min at room temperature. They were then permeabilized with 0.1% Triton X-100 for 5 min at 37°C in a CO₂ incubator, and subsequently incubated with Immunoblock (KN001; DS Pharma Biomedical, Osaka, Japan) buffer for 30 min. Fixed cells were incubated with primary antibodies for 2 h. The primary antibodies used were as follows: 1:200
growth medium into a 5-layer SCP coated with iMatrix-511TM. The hiPSCs were incubated for 3–4 days in a 5% 

analyzed using Kaluza software (Beckman Coulter).

in 1 mL PBS with 2% FBS, analyzed using a Gallios Flow Cytometer (Beckman Coulter, Brea, CA, USA), and 

100-350; Miltenyi), for 30 min on ice. The antibodies were washed with PBS, and the cells were then suspended 

( clone: REA101; 130-100-612; Miltenyi, Bergisch Gladbach, Germany), 1:10 dilution of anti-SSEA-4-PE antibodies 

PBS with 2% FBS, and each antibody was reacted at an appropriate concentration, i.e., 1:10 dilution of isotype 

β 

from day 0 to day 1, as described previously31. Cells were fixed and used for immunostaining on day 4, 7, 

FBS. To induce mesoderm, we used RPMI (Wako) with B27 minus insulin (Life Technologies) and CHIR99021 

α 

or definitive endoderm derived from hiPSCs, we used STEM Definitive Endoderm Kit (STEMCELL #05110) 

CO2 humidified atmosphere incubator at 37 °C. The medium was exchanged 2 days after seeding. The cells were 

shown in Supplementary Fig. 2 is composed of an SCP and a vibration generator. The SCP was mounted on the vibration generator and fixed by toggle clamps. A swept frequency input signal was applied to the vibration generator using a function generator (AFG-2105; TEXIO TECHNOLOGY CORPORATION, Yokohama, Japan) and an amplifier (MA1-CE; IMV Corporation, Yamanashi, Japan). hiPSCs (253G4; Kyoto University, Kyoto, Japan) were employed to evaluate of 10 passages using the RV method. hiPSCs were cultured in modified StemFit Medium22 in a 5% CO₂ humidified atmosphere incubator at 37 °C. As a control (CE), cell passage was performed by TryPLE Select (1X) (Thermo Fisher Scientific, Waltham, MA, USA) for hiPSCs with tapping. In the culture conditions of hiPSCs, we seeded 4 × 10⁷ cells into a 5-layer SCP coated with iMatrix-511TM (Nippi, Inc.). Cells at passage 4 were seeded with 100 mL growth medium into a 5-layer SCP coated with iMatrix-511TM. The hiPSCs were incubated for 3–4 days in 5% CO₂ humidified atmosphere incubator at 37 °C. The medium was exchanged 2 days after seeding. The cells were passaged 10 times and we detached cells in the same conditions as described in “Cell detachment method”.

We show the growth curve of hiPSCs during the 10 passages, immunofluorescence staining images, FCA and karyotypes with the RV/CE methods. As shown in Fig. 5a, the total cell number, N_{total} in growth curve was calculated by,

where, N_{before}, N_{detach} and N_{seed} are number of cells detached before a passage, number of detached cells and number of reseeded cells, respectively. Karyotypes of hiPSCs (Fig. 5b) were also analyzed by Nihon Gene Research Laboratories, Inc. (Sendai,16 Japan, http://www.ngrljapan.com). We conducted FCA of SSEA4 and TRA1-60, where

\[ N_{total} = N_{before} \cdot N_{detach}/N_{seed} \]

Differentiation of hiPSCs into ectoderm, mesoderm, and endoderm. To induce neural stem cells or definitive endoderm derived from hiPSCs, we used STEM Definitive Endoderm Kit (STEMCELL #05110) according to the manufacturer’s instructions. In neural cells, we induced spontaneously with MEM+ plus 5% FBS. To induce mesoderm, we used RPMI (Wako) with B27 minus insulin (Life Technologies) and CHIR99021 (Wako) from day 0 to day 1, as described previously31. Cells were fixed and used for immunostaining on day 4, 7, 3, respectively.

Measurement of flow cytometry analysis (FCA). The cells (1.0 × 10⁶ cells) were suspended in 100μL PBS with 2% FBS, and each antibody was reacted at an appropriate concentration, i.e., 1:10 dilution of isotype control (130-104-612; Miltenyi, Bergisch Gladbach, Germany), 1:10 dilution of anti-SSEA-4-PE antibodies (clone: REA101; 130-100-635; Miltenyi), and 1:10 dilution of anti-TRA-1-60-PE antibodies (clone: REA157; 130-100-635; Miltenyi), for 30 min on ice. The antibodies were washed with PBS, and the cells were then suspended in 1 mL PBS with 2% FBS, analyzed using a Gallios Flow Cytometer (Beckman Coulter, Brea, CA, USA), and analyzed using Kaluza software (Beckman Coulter).

Statistics. Values are presented as means ± SDs. Statistical significance was evaluated using Student’s t tests for comparisons between two mean values. Results with p values of less than 0.05 were considered significant.

Received: 8 October 2018; Accepted: 8 October 2019;
Published online: 30 October 2019

References
1. Takahashi, Y., Sekine, K., Kin, T., Takebe, T. & Taniguchi, H. Self-condensation culture enables vascularization of tissue fragments for efficient therapeutic transplantation. Cell Rep. 23, 1620–1629 (2018).
2. Kempf, H., Andree, B. & Zweigerdt, R. Large-scale production of human pluripotent stem cell derived cardiomyocytes. Adv. Drug Deliv. Rev. 96, 18–30 (2016).
3. Chong, J. I. H. et al. Human embryonic stem-cell-derived cardiomyocytes regenerate non-human primate hearts. Nature 510, 273–277 (2014).
4. Niebruegge, S. et al. Generation of human embryonic stem cell-derived mesoderm and cardiac cells using size-specified aggregates in an oxygen-controlled bioreactor. J. Biosci. Bioeng. 102, 493–507 (2009).
28. Hirai, H., Umegaki, R., Kino-oka, M. & Taya, M. Characterization of cellular motions through direct observation of individual cells.

29. Hayman, M. D., Blumberg, J. T., Scott, C. C. & Athanasiou, A. K. The effects of isolation on chondrocyte gene expression.

30. Tohyama, S.

31. Fewell, J. A., Patel, D., Cao, S. & Fitch, D. W. A 3D sphere culture system containing functional polymers for large-scale human pluripotent stem cell production.

32. Futcher, B. A. & Ponten, F. Regulation of cell growth and differentiation in human cell lines.

33. Fernandes, A. M. et al. Mouse embryonic stem cell expansion in a microcarrier-based stirred culture system.

34. Steindel, G. et al. Long-term microcarrier suspension cultures of human embryonic stem cells.

35. Haraguchi, Y., Matsuura, K., Shimizu, T., Yamato, M. & Okano, T. Simple suspension culture system of human iPS cells maintaining their pluripotency for cardiac cell sheet engineering.

36. Henni, N. et al. A massive suspension culture system with metabolic purification for human pluripotent stem cell-derived cardiomyocytes.

37. Kurashina, K. et al. Enzyme-free cell detachment mediated by resonance vibration with temperature modulation.

38. Kurashina, K., Takemura, T., Friend, J., Miyata, S. & Komotori, T. Efficient subculture process for adherent cells by selective collection using cultivation substrate vibration.

39. Kurashina, Y., Takemura, K., Miyata, S., Komotori, T. & Koyama, T. Effective cell collection method using collagenase and ultrasonic vibration.

40. Konagaya, S., Ando, T., Yamaguchi, T., Suemori, H. & Iwata, H. Long-term maintenance of human induced pluripotent stem cells by automated cell culture system.

41. Konagaya, S. et al. Long-term maintenance of human induced pluripotent stem cells by automated cell culture system.

42. Koyama, T., Yui, N., Koyama, M. & Koyama, H. Maintenance of human induced pluripotent stem cells by automated cell culture system.

43. Koyama, T. et al. A fully defined and scalable 3D culture system for human pluripotent stem cell expansion and differentiation.

44. Koshiba, T. et al. A fully defined and scalable 3D culture system for human pluripotent stem cell expansion and differentiation.

45. Kurashina, K., Takemura, T., Friend, J., Miyata, S. & Komotori, T. Efficient subculture process for adherent cells by selective collection using cultivation substrate vibration.

46. Kurashina, Y., Takemura, K., Miyata, S., Komotori, T. & Koyama, T. Effective cell collection method using collagenase and ultrasonic vibration.

47. Konagaya, S., Ando, T., Yamaguchi, T., Suemori, H. & Iwata, H. Long-term maintenance of human induced pluripotent stem cells by automated cell culture system.

48. Konagaya, S. et al. Long-term maintenance of human induced pluripotent stem cells by automated cell culture system.

49. Koyama, T., Yui, N., Koyama, M. & Koyama, H. Maintenance of human induced pluripotent stem cells by automated cell culture system.

50. Koshiba, T. et al. A fully defined and scalable 3D culture system for human pluripotent stem cell expansion and differentiation.

Acknowledgements
This work was mainly supported by JSPS KAKENHI Grant Numbers JP17H07081 and JP15J03923 and partially supported by the Highway Program for Realization of Regenerative Medicine of the Japan Science and Technology Agency (to K.F., 17bm054006h0007). Toshiaki Naka and Naoya Deguchi for producing the detachment machine with vibration (Shibuya Corporation). The authors thank Tomoko Haruna, Naoko Matsumoto, Sayaka Kanaami, and Yui Narita for technical assistance with cell preparation (Department of Cardiology, Keio University).

Author contributions
Y.T., Y.K., J.F. and K.T. conceived the study; Y.T., Y.K., S.T. and J.F. designed the methodologies; Y.T., Y.K. and Y.F. performed the mechanical experiments; Y.T., S.T. and Y.F. performed biological experiments and analyzed the data; Y.T., Y.K., S.T., J.F. and K.T. wrote the manuscript; J.F. and K.F. supervised the study.

Competing interests
Y.T., Y.K., S.T., K.F., J.F. and K.T. have applied for patents related to this manuscript. K.F. is CEO of Heartseed, Inc. S.T., J.F. and K.F. own equity in Heartseed, Inc. The remaining authors have no conflicts of interest to disclose.

Additional information
Supplementary information is available for this paper at https://doi.org/10.1038/s41598-019-51944-w.

Correspondence and requests for materials should be addressed to J.F. or K.T.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.
