Intelligent infusion controller with a physiological information feedback function

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Abstract.

\textbf{BACKGROUND:} In hospitals, some problems still exist, such as transfusion reaction that cannot be dealt with in time, medical staff cannot observe the physiological information of the infusion patients in real time, and the infusion speed cannot be controlled smartly.

\textbf{OBJECTIVE:} To address these problems, we propose a method for intelligent monitoring and designed a controller for dripping speed regulation.

\textbf{METHODS:} A photoelectric sensor was used to obtain the heart rate (HR) information, and a PID parameter self-tuning controller based on the fuzzy control principle was developed to establish a multi-stage adaptive control method based on HR feedback. By controlling the rotation of the motor to drive the cam to control the drip rate smartly. Also, the infusion and physiological information are transmitted to the nurse station to monitor the possible transfusion reaction.

\textbf{RESULTS:} The experiments show that the intelligent infusion controller can achieve HR signal detection with an average accuracy of over 94\%, dripping speed detection and adjustment with an average accuracy of above 98\% and adjustment time within 35 seconds.

\textbf{CONCLUSION:} Our study proved that the intelligent infusion controller can control the infusion process intelligently and effectively, and has excellent reliability, small steady-state error and high practical value.

Keywords: Infusion reaction, intelligent feedback, dripping speed control

1. Introduction

Transfusion reaction is the general term of adverse reactions associated with infusion. Although the probability of clinical occurrence is not high, the mortality rate is high if it cannot be treated in time [1,2]. On the contrary, if the transfusion reaction can be detected and handled in time, the harm of transfusion reaction to patients’ health and life safety can be reduced. At present, most hospitals use the combination of medical patrol and doctor’s recommendations to supervise the transfusion. The medical patrol will undoubtedly increase the workload of the medical staff. The way of doctor’s recommendations is to call the medical staff to carry out the corresponding infusion treatment after the patient’s subjective

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discomfort, but often the patient’s subjective feeling is lagging behind, and the best time for the infusion treatment is lost. Therefore, the development of intelligent infusion sets has become a way to solve clinical transfusion problems [3].

Intelligent infusion devices can improve the efficiency and flexibility of clinical administration and reduce the workload of medical care. However, the main problem of the current intelligent infusion devices is the low intelligence level. For example, some infusion devices can alarm the abnormal infusion speed, the end of the infusion or the emergence of bubbles in the infusion tube, but it is necessary to wait for the medical staff to carry out the infusion treatment, and the independent control of the infusion speed cannot be realized. The clinical example of Little Company of Mary Hospital in California shows that the use of the intelligent infusion device can greatly reduce the probability of common infusion problems; therefore, the intelligent and humanized infusion device has become the direction of further development [4,5].

In order to further improve the intelligence of the infusion apparatus and establish the relationship between the infusion and the physiological state of the infusion, this study proposes an intelligent infusion controller with a physiological information feedback function. It can monitor the patient’s physiological information in real time. When the physiological information (heart rate) is abnormal, it can control the infusion speed (stop or slow down the infusion speed). Through the wireless network, the transfusion information can be transmitted to the nursing station, and the abnormal transfusion can be alarmed to minimize the harm caused by the infusion reaction to the patients. The controller has a good application prospect.

2. Intelligent infusion controller design

2.1. Function and structure

The common symptoms of transfusion reaction are closely related to the heart rate (HR) of the transfusion object. This study uses the HR signal as the feedback amount of biological information to realize the intelligent adjustment of the infusion speed. As shown in Fig. 1, the intelligent infusion device mainly includes HR detection module, drip rate detection-control module, alarm module, and user interface module.

The HR detection module uses the pulse sensor photoelectric volume method to detect the HR.
method of HR measurement is based on a photonic technology, that is, when the light of a certain wavelength is irradiated to the object, the amount of light absorption is proportional to the concentration of the object [6]. The absorption and reflection of light intensity of a fixed wavelength to the surface of the skin (such as the fingertips, toes, earlobe or wrist) of a fixed wavelength is used to measure the life characteristics of the human body. This HR test is commonly used in wearable devices, such as Apple’s Apple Watch, sports watches, and some bracelets.

Drop rate detection and control module, including intelligent control algorithm and mechanical control device, are the core of intelligent infusion device. The design method is described in detail in Sections 2.2 and 2.3.

The alarm module can prompt medical staff to deal with all kinds of abnormal transfusion situations in time. The alarm mode includes missing alarm, bubble alarm and suspected infusion reaction alarm. It checks the residual liquid volume by detecting the number of drops, and notifies the doctors and nurses to change the liquid in advance. Meanwhile, the infrared tube transmitting and receiving device is used at the lower end of the infusion tube for emergency treatment. At the same time, it can also be used to detect whether there is air entry in the infusion tube. If the detected HR information is significantly different from the initial HR of the infusion, the suspected infusion response alarm will be activated.

2.2. Design of automatic control algorithm

2.2.1. The phases of the control stage

Figure 2 shows the schematic diagram of the intelligent infusion system control stage, which includes three phases.

Phase 1 of the initialization control

Before the infusion begins, the doctor sets the initial drip rate (i.e., the target drip rate \( v_0 \)), then starts the infusion, starts the timer, and starts the HR test. In this phase of three minutes, the controller adjusts the motor to control the dripping speed according to the target dripping speed and the actual dripping speed difference. At this stage, an average of 3 minutes of HR can be obtained as a reference value for HR. After three minutes, the second stage is to set the target drip rate according to the difference between
the real-time HR and its reference value. Further, the controller controls the dripping speed according to the target dripping speed and the actual dripping speed difference.

**Phase 2 of the control process**

As shown in Fig. 3, in this phase, the controller adjusts the motor’s rotation speed according to the difference between the target dropping speed and the actual dropping speed for the dripping speed control. Meanwhile, the human HR $\delta$ are monitored in real time, and the human HR is sampled and monitored within 3 minutes to obtain the average human HR, as shown below:

$$\bar{\delta} = \frac{\sum_{i=1}^{3n} \delta_i}{3n}$$

In the formula, $\delta_i$ is the HR of each sample, $n$ is the number of samples per minute, and $\bar{\delta}$ is the average human HR.

**Phase 3 of the control process**

After 3 minutes, the real-time HR monitored by the sensor determines the target drip rate through the function $f(\Delta \delta)$, so that the actual drip rate can adapt to human HR changes. The specific block diagram is shown in Fig. 4 [7].

As can be seen from Fig. 4, after 3 minutes of infusion, the real-time HR monitored by the sensor determines the target dripping speed. In this figure, $\Delta \delta$ is the ratio of the difference between the actual HR $\delta$ and the baseline HR $\bar{\delta}$ to the baseline HR, i.e.:

$$\Delta \delta = \frac{\delta - \bar{\delta}}{\delta}$$

The function $f(\Delta \delta)$ is a piecewise function, as shown below:

$$f(\Delta \delta) = \begin{cases} V & |\Delta \delta| < 0.15 \\ V/2 & 0.15 < |\Delta \delta| < 0.3 \\ 0 & |\Delta \delta| > 0.3 \end{cases}$$
According to the above formula, when the change of HR is less than 15% of the baseline HR, the infusion dripping speed is the same as the baseline dripping speed $V$. When the change in HR is 15% higher than the baseline HR, but less than 30%, the infusion rate is reduced by half, to $V/2$. When the change of HR exceeds 30% of the baseline HR, it indicates that there may be some discomfort of the patient and the infusion should be stopped immediately.

2.2.2. Control algorithm for dripping speed adjustment

The target rotation speed of the motor is determined by the difference between the target dripping speed and the actual dripping speed, and the control coefficient $(K_p, K_d)$ of the motor is determined by the fuzzy control method. The motor controls the size of the infusion port cross sectional area of the infusion tube so that the actual dripping speed keeps track of the target infusion rate.

In Fig. 4, $f(ΔV)$ is a piecewise function of the motor speed controlled by the difference between the target dripping rate and the actual dripping rate, as follows:

$$f(ΔV) = \begin{cases} ΔV > 35 \text{drops} & \text{quick rotation} \\ 4 \text{drops} \leq ΔV \leq 35 \text{drops} & \text{slow rotation} \\ ΔV < 4 \text{drops} & \text{motor stop} \end{cases}$$

Therefore, we need to determine the different motor control parameters based on the size of the drop rate difference. In view of that PID control problem of self-setting parameters in the system, a PID parameter-self-adjusting controller based on fuzzy control principle is adopted. In contrast to traditional PID control, the fuzzy PID control makes full use of the expert’s experience to construct the fuzzy rules and adjust the parameters of the controller, which can fully exert the control action of the controller, so that the whole system can be controlled better. The control block diagram is shown in Fig. 5.

It can be seen from the practical operation experience of a large number of control engineering experts that the nonlinear relationship between the three parameters of the PID controller and the system deviation $e(t)$ (expressed in e.) and the change rate of deviation $de(t)/dt$ (expressed in ec.) cannot be described by explicit mathematical expression, but this qualitative relationship can be expressed by fuzzy language [6,7]:

1. When $|e|$ is large, larger $K_p$ and smaller $K_d$ should be taken to speed up the response speed of the system and improve the tracking performance of the system. Meanwhile, the smaller $K_I$ should be adopted to limit the integration effect so as to avoid large overshoot of the system response.
2. When $|e|$ and $|ec|$ are of medium size, smaller $K_p$ should be taken to make the system overshoot a little bit smaller, the value of $K_d$ should be appropriate to ensure the response speed of the system, $K_I$ can be appropriately increased, but not too large.
3. When $|e|$ is small, $K_p$ and $K_I$ should be appropriately increased to ensure a good steady-state performance of the system, and the value of $K_d$ should be appropriate to avoid the system oscillation at the equilibrium point.
According to the actual situation of the system, the adjustment quantities of three parameters, deviation and deviation rate are divided into continuous fuzzy sets in their theoretical domain, which are generally seven: NB (negative big), NM (negative middle), NS (negative small), ZO (zero), PS (positive small), PM (positive middle) and PB (positive big) [8,9]. According to the experience summarized above, the fuzzy rules governing three parameters of the PID controller are formulated, such as:

If $e$ is NB and $ec$ is NB, Then $\Delta K_p$ is PB

Specific rules of the fuzzy PID controller are shown in Tables 1 and 2. According to the specific conditions of $e$ and $ec$ and the fuzzy rules in the table, the fuzzy PID controller can determine the adjustment amount of parameters at each time corresponding to the fuzzy set, adjust the parameters of the PID controller in real time, and get the parameters at the next time (only PD control is used here):

$$K_p = K_p + \Delta K_p, \quad K_d = K_d + \Delta K_d$$

2.3. Mechanical design of the controller

The mechanical part of the infusion controller is the carrier to realize the infusion control, and the main structures include a Murphy’s burette slot, a drip-speed control unit, a drip-speed sensor and a bubble sensor mounting holes. The drip-speed control unit consists of a rotating CAM and baffle, through which the drip tube at the back of the Murphy’s burette is passed. The CAM controlled by the motor can adjust the clamping degree of the drip tube through rotation, so as to control the drip speed. The mechanical structure and physical objects are shown in Fig. 6.

2.4. Wireless network system for infusion monitoring [10–13]

Based on the design of the intelligent infusion controller with a physiological information feed-
Fig. 6. Mechanical structure and physical objects of the infusion controller.

Fig. 7. The remote wireless infusion monitoring system networking framework.

back function, it can be further extended to a wireless infusion monitoring system, and its networking framework is shown in Fig. 7. It is mainly composed of the upper computer, coordinator, routes and terminals. The upper computer receives and displays the patient’s infusion physiological information and infusion speed and other information transmitted by the coordinator in real time, and can also set the patient’s infusion speed through the keyboard, and alarm if there is any abnormality. The coordinator transmits the patient’s infusion physiological information and infusion speed and other information sent by the terminals (or routers) through the wireless network to the upper computer, and sends the instructions of the upper computer to the terminals through the wireless network [14,15]. The terminal should have the following basic modules: the infusion speed detection module, the infusion speed control module, the patient’s physiological information acquisition module, the keypad module, the display module, the wireless networking module and the alarm module. The route has the functions of the terminal, and can forward the terminal information to the coordinator, which extends the network coverage.
Table 3
Records of dripping speed setting value and actual value

| Test number | 1 | 2 | 3 | 4 | 5 |
|-------------|---|---|---|---|---|
| Setting dripping speed | 40 | 60 | 80 | 100 | 120 |
| Dripping speed measured by sensor | 40 | 60 | 80 | 100 | 120 |
| Error | 0 | 0 | 0 | 0 | 0 |

Table 4
Time records of adjusting the dripping speed

| Initial dripping speed (drops/min) | Target dripping speed (drops/min) | Adjustment time (sec) | Initial dripping speed (drops/min) | Target dripping speed (drops/min) | Adjustment time (sec) |
|-----------------------------------|-----------------------------------|-----------------------|-----------------------------------|-----------------------------------|-----------------------|
| 80                                | 120                               | 21                    | 40                                | 80                                | 21                    |
| 80                                | 100                               | 18                    | 40                                | 100                               | 23                    |
| 80                                | 60                                | 15                    | 40                                | 120                               | 30                    |
| 80                                | 40                                | 19                    | 20                                | 40                                | 38                    |
| 80                                | 20                                | 32                    | 20                                | 60                                | 25                    |
| 40                                | 20                                | 28                    | 20                                | 80                                | 30                    |
| 40                                | 60                                | 19                    | 20                                | 100                               | 31                    |

3. Results

3.1. HR detection

First, the HR algorithm is validated by ECG signal generator. The HR output range is set 30 to 300. Through 20 sets of data tests, the recognition accuracy of our HR algorithm is 98%. In addition, 30 volunteers (aged 10–65 years) were selected for further human experiment verification, and the HR detection module was compared with Colin n1bp-88s monitor (Colin Corporation, Japan). The results show that the detection accuracy of HR detection module is over 94%, which can provide a basis for the judgment of infusion response.

3.2. Dripping speed detection

In order to evaluate the accuracy of the sensor in measuring the dripping speed, the sensor dripping speed measurement was compared with the manual measurement, and the stopwatch was used to time the measurement of the manual drop rate. In 30 tests, the dripping speed was set 30 to 150, and the average accuracy of the sensor dripping speed measurement is over 98%.

3.3. Dripping speed control

3.3.1. Comparison of the target dripping speed (setting dripping speed) with actual dripping speed

After manually setting the dripping speed and then waiting for the end of the system speed regulation, the dripping speed measured by the sensor is compared with the set dripping speed. There results after several measurements are shown in Table 3. According to the test data, the intelligent infusion system can accurately control the dropping speed of the infusion system to reach the set target value in five tests. Combined with the experimental results of the sensor dropping speed detection (the average coincidence rate of dropping speed > 98%), the actual average adjustment accuracy of the set dropping speed control is more than 98%.
3.3.2. Adjustment time to achieve target dripping speed

The intelligent infusion system has a certain initial dripping speed. After manually setting the dripping speed, the intelligent infusion system will automatically adjust the speed, and wait for the sensor to stabilize to the target dripping speed and analyze the adjustment time. The results after several measurements are shown in Table 4. The test shows that the intelligent infusion system can quickly and accurately control the dropping speed of the infusion system to reach the set target value. When the target dropping speed is the same, the less the absolute error between the initial dropping speed and the target dropping speed is, the less adjusting time the intelligent infusion system needs. When the initial dropping speed is the same, the less the absolute error between the initial dropping speed and the target dropping speed is, the less adjusting time the intelligent infusion system needs.

4. Discussion and conclusion

Intravenous infusion is the most common medical method in clinical treatment. In view of the problems of inaccurate control of traditional infusion drip rate, inappropriate detection and treatment of infusion reaction, and inability of real-time monitoring of physiological information of infusion patients, this design proposes a monitoring and control method of infusion drip rate with physiological information feedback, which can be used in 35 seconds. The accuracy rate of the dripping speed is over 98%, and the accuracy of the HR signal detection reaches 94%. The fuzzy PID compound controller is used to control the dropping speed of the infusion, which effectively solves the nonlinear relationship between the dropping speed and the height of the liquid and improves the steady-state accuracy of the system.

The intelligent infusion control system designed in this paper realizes the centralized monitoring of patients’ infusion information and physiological information. The functions of dripping speed control and HR detection can fully meet the basic requirements of general large and medium-sized infusion rooms or hospitals. The sound and light alarm function can prompt medical staff to deal with patients’ lack of fluid and suspected infusion reaction situation in time. Experiments show that the intelligent infusion control system has stable performance, reliability, small steady-state error and high practical value.

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Conflict of interest

None to report.

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