Optimal resolution in Fresnel incoherent correlation holographic fluorescence microscopy

Gary Brooker,1,2* Nisan Siegel,1,2 Victor Wang,1,2 and Joseph Rosen1,2,3,4

1Department of Biomedical Engineering, Johns Hopkins University, 9605 Medical Center Drive, Rockville, Maryland 20850 USA
2Microscopy Center, Johns Hopkins University Montgomery County Campus, Rockville, Maryland 20850 USA
3Department of Electrical and Computer Engineering, Ben-Gurion University of the Negev, P.O. Box 653, Beer-Sheva 84105, Israel
4rosen@ee.bgu.ac.il
*gbrooker@jhu.edu

Abstract: Fresnel Incoherent Correlation Holography (FINCH) enables holograms and 3D images to be created from incoherent light with just a camera and spatial light modulator (SLM). We previously described its application to microscopic incoherent fluorescence wherein one complex hologram contains all the 3D information in the microscope field, obviating the need for scanning or serial sectioning. We now report experiments which have led to the optimal optical, electro-optic, and computational conditions necessary to produce holograms which yield high quality 3D images from fluorescent microscopic specimens. An important improvement from our previous FINCH configurations capitalizes on the polarization sensitivity of the SLM so that the same SLM pixels which create the spherical wave simulating the microscope tube lens, also pass the plane waves from the infinity corrected microscope objective, so that interference between the two wave types at the camera creates a hologram. This advance dramatically improves the resolution of the FINCH system. Results from imaging a fluorescent USAF pattern and a pollen grain slide reveal resolution which approaches the Rayleigh limit by this simple method for 3D fluorescent microscopic imaging.

©2011 Optical Society of America

OCIS codes: (110.0180) Microscopy; (090.1995) Digital holography; (180.2520) Fluorescence microscopy; (180.6900) Three-dimensional microscopy; (050.1950) Diffraction gratings; (090.1760) Computer holography; (090.1970) Diffractive optics; (090.2880) Holographic interferometry; (100.6890) Three-dimensional image processing; (110.6880) Three-dimensional image acquisition; (120.5060) Phase modulation; (260.2510) Fluorescence; (330.1720) Color vision.

References and links
1. B. W. Schilling, T.-C. Poon, G. Indebetouw, B. Storrie, K. Shinoda, Y. Suzuki, and M. H. Wu, “Three-dimensional holographic fluorescence microscopy,” Opt. Lett. 22(19), 1506–1508 (1997).
2. J. Rosen and G. Brooker, “Non-Scanning Motionless Fluorescence Three-Dimensional Holographic Microscopy,” Nat. Photonics 2(3), 190–195 (2008).
3. O. Mudanyali, D. Tseng, C. Oh, S. O. Isikman, I. Sencan, W. Bishara, C. Oztoprak, S. Seo, B. Khademhosseini, and A. Ozcan, “Compact, light-weight and cost-effective microscope based on lensless incoherent holography for telemedicine applications,” Lab Chip 10(11), 1417–1428 (2010).
4. E. Y. Lam, X. Zhang, H. Vo, T.-C. Poon, and G. Indebetouw, “Three-dimensional holographic microscopy and sectional image reconstruction using optical scanning holography,” Appl. Opt. 48(34), H113–H119 (2009).
5. G. Indebetouw, Y. Tada, J. Rosen, and G. Brooker, “Scanning holographic microscopy with resolution exceeding the Rayleigh limit of the objective by superposition of off-axis holograms,” Appl. Opt. 46(6), 993–1000 (2007).
6. J. Rosen and G. Brooker, “Digital spatially incoherent Fresnel holography,” Opt. Lett. 32(8), 912–914 (2007).
7. J. Rosen and G. Brooker, “Fluorescence incoherent color holography,” Opt. Express 15(5), 2244–2250 (2007).
8. J. W. Goodman, Introduction to Fourier Optics, 2nd ed. (McGraw-Hill, 1996).
9. C. Maurer, A. Jesacher, S. Bernet, and M. Ritsch-Marte, “What spatial light modulators can do for optical microscopy,” Laser Photonics Rev. 5(1), 81–101 (2011).
1. Introduction

Incoherent [1,2] and partially coherent [3] digital holographic microscopies have recently become fields of much interest because of the ability of microscopes based on these principles to image three dimensional (3D) incoherent objects. In addition, some of these systems are capable of imaging fluorescent labeled specimens [1,2], while others can perform sectioning of the 3-D observed volume [4]; and some have even demonstrated improvement in resolution by operating in synthetic aperture mode [5]. More recently, a lensless version of a partially coherent [3], digital holographic microscope has been installed on-chip in a very compact configuration. The potential of these technologies is promising.

The holographic method used in this study is based upon the recently invented system of a single-channel incoherent interferometer employed for generating digital Fresnel holograms [6,7]. In this non-scanning holographic technique, incoherent light is reflected or emitted from a 3D object, then propagates through a spatial light modulator (SLM), and is finally recorded by a digital camera. For every source point the SLM is used as a diffractive beam splitter in an incoherent interferometer, so that each spherical beam, originating from each object point, is split into two spherical beams with two different curve radii. Accumulation of the entire interferences for all of the couples of spherical beams creates the Fresnel hologram of the observed object. Three holograms are recorded sequentially, each for a different phase factor of the SLM, and are superposed during data processing to produce a complex-valued Fresnel hologram free of the twin image and bias term.

In theory, optical microscopy lends itself to readily adapt the FINCH principle, since the light emitted from an infinity corrected objective is a plane wave that is then focused to an image plane by the microscope tube lens. The FINCH principle can be applied by substituting an SLM for the tube lens to create the spherical wave along with passing the plane wave to the camera, so that there is interference between the two coincident beams [2]. Recording of this interference on a CCD camera creates a hologram of the specimen.

In the present study we have examined the factors necessary to obtain optimal resolution in fluorescence microscopy with the FINCH technique. We report here the combination of a number of new advances in FINCH microscopic imaging which has yielded resolution which approaches the Rayleigh limit.

2. Materials and methods

2.1 Microscope and optical setup

The experimental microscope system was configured as shown in Fig. 1 on a Zeiss Axioskop 2FS microscope platform using an Olympus × 20 - 0.75 NA objective. In the majority of the experiments, the test subject was a negative USAF test slide (Edmund Optics 59204) which rested on a fluorescent plastic backing slide (Chroma) so that the clear features were fluorescent. We also imaged Mixed Pollen Grains (Carolina Biological 30-4264). Either a GFP or Cy3 filter set (Semrock) was used. The correct working distance between the objective and specimen was quite critical and established by first bringing the sample into focus by viewing the specimen through the microscope binoculars. Once the correct focus was established, it was kept constant, the tube lens and binocular were removed and the holography configuration shown in Fig. 1 was established. Because the SLM functions as the tube lens of the microscope, creating the spherical wave along with passing the plane wave to the camera, the current configuration contains a non-polarizing beam splitting cube so that the SLM is optically on axis to eliminate any possibility of image distortion from the SLM lens.
pattern. In our previous configuration of the microscope for FINCH holography, which we called FINCHSCOPE [2], the SLM was positioned at an angle and we made simple corrections to the lens patterns displayed on the SLM to minimize distortions. In the present configuration, the lens patterns are normal to the optical plane, so that no corrections are necessary and no distortion or loss of resolution can be attributed to having the SLM at an angle to the optical axis. The distance that the light traveled through the beam splitting cube was 25 mm, and the distance between the cube and SLM was 4 mm. The distance between the back aperture of the objective and SLM was 130 mm. The distance between the SLM and camera (QImaging Cooled Retiga 4000R, 2,048 × 2,048 pixel 12-bit CCD sensor) was varied between 164.5 mm and 800 mm, with the optimal distance $z_h$ (see Fig. 5) being 400 mm.

![FINCHSCOPE with ON-AXIS REFLECTIVE SLM](image)

Fig. 1. Microscope configuration for holographic imaging. A fluorescent slide was positioned on the stage of the microscope and illuminated by standard epifluorescence methods. The illumination was controlled with a shutter to minimize photobleaching. The fluorescence emission passed through an input polarizer aligned with some angle to the polarization sensitive axis of the SLM. The emission beam reflected off of the SLM containing the appropriate diffractive lens patterns and then through an output polarizer before reaching the CCD camera.

The laser beams were directed into the microscope through a beam splitting cube attached to the microscope turret as shown in Fig. 2, and used for a variety of functions including precisely aligning the system and measuring the SLM performance.
Fig. 2. Microscope configuration for SLM testing and alignment. A Coherent DPSS 532 nm or Thorlabs 633 nm laser passed through a Glan-Thompson polarizer and 20 x beam expander. The expanded laser beam was confirmed to be coherent and collimated with a shearing plate interferometer. The beam was directed to the microscope through a beam splitting cube mounted on the microscope turret which allowed the expanded laser beam to enter the microscope, reflect off the SLM and be directed to the camera or in some cases a power meter. Moving the turret to another position with a microscope objective made it possible to first obtain precision alignment of the microscope using the lasers and then to switch to imaging mode with objectives. The distance between the camera and SLM \((z)\) was varied by moving the camera along a precision track to confirm the focal lengths and characteristics of diffractive lens patterns.

2.2 Spatial light modulator configuration, Fresnel patterns and polarizers

In the original configuration of FINCHSCOPE, a diffractive lens phase pattern was displayed on the SLM, creating a random composition of two different lenses. In the experiments reported here, 37% of the pixels were randomly selected; along with the 13% of the SLM surface that is never active in light modulation (fill factor). These pixels had very long (8.2 m) focal length, in essence focusing slightly the plane wave of every object point from the objective; for the sake of convenience, this wave is still referred to as the plane wave. The rest of the SLM pixels displayed a quadratic phase mask. Therefore, a single wavefront originating from any object point was split by the SLM into two mutually coherent wavefronts with two different spherical curves. These two beams propagate in the same direction toward the camera and mutually interfere on the CCD sensor chip, creating the holographic image. In a new approach reported here that takes advantage of the polarization properties of the SLM, it is possible to utilize the same pixels to pass both the mutually coherent plane and spherical waves by using input and output polarizers (Thorlabs LPVIS100) before and after the light from the objective is reflected off of the SLM. The ‘input’ polarizer, placed in the optical path before the SLM, serves to transmit plane wave from the objective to the SLM with polarization components both aligned with and orthogonal to the SLM polarization, of which every pixel displays the quadratic phase mask. The component with polarization aligned with that of the SLM is focused into a spherical wave, while the component with polarization orthogonal to that of the SLM is simply reflected as if from a mirror. The ‘output’ polarizer, which is the last optical component in the optical path before the CCD, passes both spherical
wave and plane wave with identical polarization. These two waves then propagate toward the CCD, interfere with one another and thus create the holographic image which is recorded by the CCD, as in the original FINCHSCOPE configuration. The center of the SLM (and the diffractive lens pattern) was precisely aligned with the optical axis of the microscope system.

![Graph](image)

Equation for 532 nm laser: \( y = 127480x + 15.171 \)

Equation for 633 nm laser: \( y = 109084x + 8.8986 \)

Fig. 3. Relationship between the radial parameter of the displayed quadratic phase patterns on the SLM at 532 nm and 633 nm and the distance of the measured plane of focus. Lines marked linear represent best fit lines calculated by the least squares method. The equations for the best fit lines are included.

Application of quadratic phase patterns \( \exp\left[-i\pi F_L (x^2 + y^2)\right] \) to the SLM resulted in a primary plane of focus according to the lens transfer function [8], \( \exp\left[-i\pi \left(x^2 + y^2\right)/\lambda f_d\right] \) where \( \lambda \) is the wavelength and \( f_d \) is the focal length of the diffractive lens displayed on the SLM. Figure 3 demonstrates the functionality of the SLM as a diffractive spherical lens under illumination of two different laser beams with two wavelengths. Equating the argument of the lens transfer function for full aperture of the SLM to the argument of the digital phase pattern and isolating the focal length yields the following equation for the focal length,

\[
f_d = \frac{\Delta^2 N^2}{4\lambda x_{\text{max}}^2 F_L}, \tag{1}
\]

where \( \Delta \) is the pixel size, \( N \) is the number of pixels along the largest dimension of the SLM and \( x_{\text{max}} \) is the value of the matrix \((x, y)\) at the points \((\pm N/2, 0)\) (for the experiments reported here, \( \Delta = 8 \mu m, N = 1920 \) and \( x_{\text{max}} = 0.873 \)). Substituting the SLM parameters into Eq. (1) gives the equations \( f_d = 145473/F_L \) and \( f_d = 145473/F_L \) for \( \lambda = 532 \text{ nm} \) and \( 633 \text{ nm} \), respectively.
respectively. This is a difference between the calculated and experimental data in the slopes of
the graphs in Fig. 3 of about 12.5% and 11% for \( \lambda = 532 \text{ nm} \) and \( 633 \text{ nm} \), respectively. The
reflective SLM devoid of any pattern has a slight curvature for which we measured a focal
length of \( f_{\text{SLM}} = 8.2 \text{ meters} \). Taking this into account, the total measured focal length \( f_m \) is
calculated as the focal length of two successive lenses:

\[
f_m = \frac{f_d f_{\text{SLM}}}{f_d + f_{\text{SLM}}} = \frac{c f_{\text{SLM}}}{c + f_{\text{SLM}}} \tag{2}
\]

where \( c \) is the slope of the linear curve \( f_d (1/F_L) \cdot f_m (1/F_L) \) is no longer a linear curve but for
\( f_{\text{SLM}} \gg f_{\text{d,max}} \) it can be approximated to a linear curve with an average slope \( c_a \) of

\[
c_a = \frac{c f_{\text{SLM}}^2}{F_{L,mid} \left( \frac{c}{F_{L,mid} + f_{\text{SLM}}} \right)} \tag{3}
\]

where \( F_{L,mid} \) is the middle value of the range of \( 1/F_L \), which in the present experiment is equal
to \( F_{L,mid} \approx 244 \). Substituting the parameters \( f_{\text{SLM}} = 8.2 \text{m} \), \( F_{L,mid} = 244 \), \( c(\lambda = 532 \text{ nm}) = 145473 \)
and \( c(\lambda = 633 \text{ nm}) = 122262 \) into Eq. (3) gives modified values for the slopes of \( c_a(\lambda = 532 \text{ nm}) = 126421 \)
and \( c_a(\lambda = 633 \text{ nm}) = 108586 \). After accounting for the inherent curvature of
the SLM, the difference between the calculated and experimental data in the slopes of the
graphs in Fig. 3 is only 0.83% and 0.46% for \( \lambda = 532 \text{ nm} \) and 633 nm, respectively, which is
within measurement error.

The SLM used was a phase-only SLM (Holoeye HEO 1080P; 1080 × 1920 pixels). The
\( z_h \) distance used (400 mm) for the images reported here was greater than the 230 mm
calculated minimum focal length of the SLM. The minimum focal length is determined by the
SLM's pixel size \( \Delta \) (8 microns), and the number of pixels \( N \) (1920) along the SLM's diameter,
according to the inequality \( f_d \geq N \Delta^2/\lambda \). The SLM firmware was modified and confirmed to
produce the desired focal lengths and phase shifts (using 532 nm and 633 nm coherent
collimated and expanded laser beams for calibration and testing) to deliver a full \( 2\pi \) phase
shift over its working range of 256 gray levels. Diffractive lenses such as the lens patterns on
this SLM will have multiple higher diffraction order foci in the desired focal plane, as well as
other, undesired, focal planes at different focal distances than the desired focal plane. In the
configuration used here, the focusing efficiency of the SLM into the central image of the
desired focal plane was measured to be greater than 50%, with insignificant intensity
concentrated in undesired planes of focus. Furthermore, at the camera-SLM distance of 400
mm, the higher diffraction order images in the desired focal plane did not project onto the
CCD. Recently an excellent review \[9\] has appeared which describes the characteristics of
SLM devices and their application to a variety of functions in microscopy.
Fig. 4. Comparison of using a constant phase mask (a) versus the polarization method (b) to select and separate the plane and spherical waves in FINCH holography. Notice that when the polarization method is used, all the pixels on the SLM are used to create the diffractive lens pattern.

2.3 Computational methods

In the current FINCH configuration, the creation of a complex hologram and its reconstruction involves a number of steps. The complete process for microscopic imaging has been automated with computer programs written in LabVIEW (National Instruments). The first step includes a cycle of creating the appropriate quadratic phase mask and applying it to the SLM, opening the shutter to illuminate the sample and capturing a hologram and repeating this cycle for quadratic phase patterns wherein the phase shift is changed between $\theta_k = 1, 2, 3 = 0, 120$ and $240$ degrees [2]. Next, the three holograms are superposed to create a complex hologram on which Fresnel propagation is performed to yield the individual image planes in the sample. In the case of the USAF test target the best reconstructed plane of focus was selected.
3. Theoretical considerations

FINCH creates holograms in a single beam system as a result of interference between a plane wave and a spherical wave originating from every object point. In our previous reports we created a random constant phase mask so that with a phase-only SLM, the plane wave from an infinity corrected microscope objective could be directed to the camera along with the spherical wave created by the SLM. The use of a constant phase mask presents certain disadvantages in that it requires half the pixels on the SLM and also degrades the resolution of the mask which creates the spherical wave. Because only one linear polarization state on the liquid crystal based SLM can change the phase of incoming light, half of the randomly polarized fluorescent light striking the device can have quadratic phase modulation whereas the other half is shifted by a constant phase, as shown in Fig. 4(a). However, the sensitivity of the SLM to a specific linear polarization also makes it possible to use the portion of the light not affected by the SLM to deliver the plane wave as shown in Fig. 4(b), and discussed earlier and below.

The following analysis refers to the system scheme shown in Fig. 5, where it is assumed that the object is an infinitesimal point and therefore the result of this analysis is considered as a point spread function (PSF). For an arbitrary object point at \( (\vec{r}, -z_s) \), in a working distance \( z_s \) before the objective, where \( \vec{r} = (x_s, y_s) \), the complex amplitude beyond the first polarizer, just before the SLM, is

\[
    u_o(x_o, y_o) = C_1(\vec{r}_z) \exp \left( \frac{-\vec{r}}{z_s} \right) \frac{1}{Q(\frac{1}{z_s})} \frac{1}{Q(\frac{-1}{f_o})} \frac{1}{Q(\frac{1}{d_i})} \left( A_x \hat{x} + A_y \hat{y} \right) \tag{4}
\]

Fig. 5. Microscope scheme. \( P_1, P_2 \) are the polarizers.
where it is assumed that the polarizer axis is tilted in a $\phi_1$ angle to the $x$ axis, $f_o$ is the focal length of the objective, $d_i$ is the distance between the objective and the SLM and $A_o, A_i$ are the constant amplitudes in the $x, y$ axes, respectively. The asterisk denotes a two dimensional convolution and $\hat{x}$ and $\hat{y}$ are unit vectors in the $x, y$ directions, respectively. For the sake of shortening, the quadratic phase function is designated by the function $Q$, such that

$$Q(b) = \exp\left[ i \pi b \lambda^{-1} \left( x^2 + y^2 \right) \right] \quad \text{and} \quad C_{1}(\tau)$$

is a complex constant dependent on the source point's location. The SLM modulates the light in only a single linear polarization and in our case, without loss of generality, this axis is chosen to be $x$. The light polarized in $y$ direction is reflected from the SLM with only a constant phase shift. Therefore the complex amplitude on the output plane of the SLM is,

$$u_i(x_i, y_i) = C_1(\tau) L \left( \frac{-\tau}{z_s} \right) Q \left( \frac{1}{z_s} \right) Q \left( \frac{-1}{f_o} \right) * Q \left( \frac{1}{d_i} \right)$$

$$\times \left[ A_i B_o \exp(i\theta) Q \left( \frac{-1}{f_o} \right) \hat{x} + A_i B_o \hat{y} \right]$$

(5)

where $B_o$ and $B_i$ are complex constants. $\theta$ is one of the three angles used in the phase shift procedure in order to eliminate the bias term and the twin image [6,7]. The complex amplitude after passing the second polarizer, with axis angle of $\phi_2$ to the $x$ axis, has linear polarization in the direction of the polarizer axis. Therefore we can abandon the vector notation and express the complex amplitude beyond the second polarizer, on the CCD plane, as

$$u_z(x_z, y_z) = C_1(\tau) L \left( \frac{-\tau}{z_s} \right) Q \left( \frac{1}{z_s} \right) Q \left( \frac{-1}{f_o} \right) * Q \left( \frac{1}{d_i} \right)$$

$$\times \left[ A_i B_o \sin\phi_2 + A_i B_o \exp(i\theta) Q \left( \frac{-1}{f_o} \right) \cos\phi_2 \right] * Q \left( \frac{1}{z_h} \right)$$

(6)

where $z_h$ is the distance between the SLM and the CCD. The intensity of the recorded hologram is,

$$I_p(x_z, y_z) = \left| C_1(\tau) L \left( \frac{-\tau}{z_s} \right) Q \left( \frac{1}{z_s} \right) Q \left( \frac{-1}{f_o} \right) * Q \left( \frac{1}{d_i} \right) \right|^2$$

$$\times \left[ A_i B_o \sin\phi_2 + A_i B_o \exp(i\theta) Q \left( \frac{-1}{f_o} \right) \cos\phi_2 \right] * Q \left( \frac{1}{z_h} \right)$$

(7)

Following the calculation of Eq. (7), the intensity on the CCD plane is,

$$I_p(x_z, y_z) = \left( C_1 + C_1(\tau) Q \left( \frac{1}{z_s} \right) L \left[ \frac{-\tau}{z_s} \right] \exp(i\theta) + C_1(\tau) Q \left( \frac{-1}{z_s} \right) L \left[ \frac{-\tau}{z_s} \right] \exp(-i\theta) \right)$$

$$= A_i \left[ 2 + \exp \left\{ i \pi \lambda \left\{ \left( x_z - \frac{z_h f_x x_i}{z_i (f_x + d_i)} \right)^2 + \left( y_z - \frac{z_h f_y y_i}{z_i (f_x + d_i)} \right)^2 \right\} \right\} + i\theta \right]$$

$$+ \exp \left\{ -i \pi \lambda \left\{ \left( x_z - \frac{z_h f_x x_i}{z_i (f_x + d_i)} \right)^2 + \left( y_z - \frac{z_h f_y y_i}{z_i (f_x + d_i)} \right)^2 \right\} \right\} - i\theta \right\}.$$
where $A_o, C_2, C_3$ are constants and $z_r$, the reconstruction distance of the object point, is given by

$$z_r = \pm \left( \frac{f_1 + z_h}{f_1 - f_z - d_i} \right) \left( \frac{f_x + d_i}{f_1 - \left( f_x + d_i \right)} \right),$$

where $f_1 = \frac{f_x (f_x + d_i)}{f_d - \left( f_x + d_i \right)}$ and $f_x = \frac{z_h f_o}{\left( f_o - z_r \right)}$. \hspace{1cm} (9)

The transverse location of the reconstructed object point is,

$$\vec{r}_t = \vec{r}_s - \frac{z_h f_x}{z \left( f_x + d_i \right)},$$

where $\vec{r}_s = (x_s, y_s)$. \hspace{1cm} (10)

Equation (8) is the typical expression of an on-line Fresnel hologram of a single point and therefore $I_p(x_2, y_2)$ is the PSF of the recording part of the FINCH. To avoid the problem of the twin image, one of the interference terms, (the second or third terms) in Eq. (8) should be isolated by the phase-shifting procedure [10,11]. Reconstructing this term by Fresnel back propagation yields the image of the point at a distance $z_r$ from the hologram given by Eq. (9), and at a transverse location $\vec{r}_t = (x_t, y_t)$ given by Eq. (10). The sign '$\pm$' in Eq. (9) indicates the possibility to reconstruct from the hologram either the virtual or the real image depending on which term, second or third, is chosen from Eq. (8). The polarization angles $\phi_1$ and $\phi_2$ are chosen in order to maximize the interference terms [the second and third terms in Eq. (8)]. Their precise values depend on the values of the constants $|B_Q|$ and $|B_M|$. In this study we choose their values empirically by picking the angles that yield the best reconstructed image.

Based on Eq. (10), the transverse magnification of this FINCH system is

$$M_T = \frac{\partial \vec{r}_t}{\partial r_s} = \frac{z_h f_x}{z \left( f_x + d_i \right)}.$$ \hspace{1cm} (11)

In this stage we can simplify Eqs. (8) – (11) by choosing the working distance to be $z_h = f_o$, as was indeed chosen in the present experiment. In this case $f_o \to \infty$, and therefore $f_1 = f_o$, $z_r = \pm (z_h f_d)$ and $M_T = z_h / f_o$.

The minimal resolved object size observed by reconstructing the FINCH hologram is dictated by either the input or output apertures according to the following equation

$$\Delta_{\min} = \max \left\{ \frac{\lambda}{NA_{in}}, \frac{\lambda}{\left( M_T NA_{out} \right)} \right\} = \max \left\{ \frac{2 \lambda}{D_{SLM}}, \frac{2 \lambda}{\left( M_T D_H \right)} \right\}, \hspace{1cm} (12)$$

where $D_{SLM}$ and $D_H$ are the diameters of the SLM, and the recorded hologram, respectively. $NA_{in}$ and $NA_{out}$ are the numerical apertures of the system input and output, respectively. The $NA_{in}$ is independently determined by the objective and cannot be changed by the design of the FINCH system. However the product $NA_{out} M_T$ is dependent on the system parameters and our goal should be to keep this product equal or larger than $NA_{in}$ in order not to reduce the resolution determined by the input aperture. Therefore, referring to Eq. (12), an optimal FINCH system satisfies the inequality,

$$f_x / D_{SLM} \geq \left| z_h / \left( M_T D_H \right) \right|.$$ \hspace{1cm} (13)

In this inequality all the parameters are well defined besides the diameter of the hologram. This size is dependent on the overall size of the reconstructed image. Based on simple geometrical considerations the diameter of the hologram is,

$$D_H = D_{SLM} \left| \frac{\left( 1 - a \right) z_h}{f_d} \right|,$$ \hspace{1cm} (14)
where \( a \) is the ratio between the image and the SLM sizes. \( a \) ranges between almost zero for an image of a point, to 1 for a full frame image. Substituting Eq. (14) and quantities \( z_r = |f_d - z_h| \) and \( M_r = z_h/f_d \) into Eq. (13) yields

\[
1 \geq \frac{f_d - z_h}{z_h \left(1 - (1 - a) z_h/f_d\right)}.
\]

The only free parameter in this analysis that does not influence other performances of the system is \( f_d \). Therefore by calculating the inequality in Eq. (13) we find the optimal \( f_d \) in sense of best image resolution. The solution of Eq. (15) is \( f_d \leq \frac{1}{1 + \sqrt{a}} z_h \). In this study and in Ref [11], we used the complete field of view, and therefore we assume \( a = 1 \). Consequently the focal length of the diffractive lens should be equal or smaller than twice the distance between the SLM and the CCD, or in a formal way, \( f_d \leq 2z_h \). Because the CCD chip is not ideal as a medium for hologram recording, practically it is optimal to display the image as far as possible from the CCD chip. Therefore we find that \( f_d = 2z_h \) is the optimal choice for the length of the focal length of the diffractive lens.

4. Results

The optimal conditions for imaging the fluorescent USAF slide with both the constant phase mask method and the polarization method were compared. The results demonstrate the superiority of the polarization method. Figure 6 shows the optimal plane of focus from image reconstructions made from holograms captured with both methods. The conditions were identical, using an 800 mm focal length diffractive lens pattern and with the camera positioned 400 mm from the SLM. In Fig. 6(a) the holograms were captured with a 37\% constant phase mask and with the input and output polarizers set at 0 degrees (i.e. parallel with the SLM polarization). In Fig. 6(b) the holograms were captured using the polarization method, without any constant phase mask and with the polarizers set at 60 degrees to the \( x \) axis.

Fig. 6. Best plane of focus reconstruction from holograms of the fluorescent USAF test slide using the constant phase mask technique and the polarizers method. (a) Static mask. (b) Input and output polarizers at 60 degrees. Olympus 20 \( \times \) 0.75 NA objective. Bars labeled “a” are 1.6 microns thick and there is 2.5 microns distance between each of the three bars. Full bin 1 camera field of view, 300 microns square.

Imaging pollen grains has been a convenient way to compare the performance of microscopes on biological samples. We compared the performance of the new dual-polarizers method to our previous constant phase mask method. As with the USAF slide, the results with
the polarizers method were much better for the exact same field as shown in Fig. 7. Also notice the improved resolution of the two pollen grains along the edges of the field with the polarization method. The slight ghost images that can be seen in Fig. 6 are not inherent to FINCH, because ghost images have been viewed even when the SLM has been used as a flat mirror or even when it has been replaced by a regular flat mirror and a refractive lens (data not shown). We suspect that these ghost images appear because of light reflections from the beam splitter. There were no ghost images in images taken with a 45° flat mirror and refractive lens, but that configuration was not suitable for FINCH.

Another advantage of the FINCH holographic method for capturing a 3D image is that the reconstructed image planes have much less out of focus haze when compared to widefield microscopy. This phenomenon can be explained by the following. A widefield microscope has a single PSF which becomes wider and weaker when propagating far from the image plane. A holographic microscopic imager like those using FINCH is different. Each transverse section has its own PSF which is similar to that of the widefield PSF. Therefore every section along the z axis is sharply imaged, i.e. convolved with a relatively sharp PSF of the relevant section, and is summed with relatively weak haze contributed from the other out of focus sections.

The effect of input and output polarization upon reconstructed best planes of focus was tested after capturing holograms of the fluorescent USAF slide for a matrix of conditions wherein the input and output polarization was varied in 15 degree increments between 0 and 90 degrees. Figure 8 shows the phase 0° holograms from each condition and Fig. 9 shows the best plane of focus which was reconstructed from these (and their associated 120° and 240° phase-shifted) holograms. It can be seen that the best conditions for recording holograms were with input and output polarization combinations varying between 45 and 60 degrees.
Fig. 8. Holograms of the USAF fluorescent test slide using an Olympus 20 × 0.75 NA objective. The input and output polarization orientation was changed as shown in the matrix and the phase 0° hologram from each series of three holograms (phase 0°, 120° and 240°) is shown.
The best plane of focus from reconstructions of holograms of the USAF fluorescent test slide using an Olympus 20 × 0.75 NA objective is shown. The input and output polarization orientation varied as indicated.

The effect of the fluorescence emission bandwidth on widefield images and those generated by FINCH holography was examined. The emission bandwidth of the Semrock GFP filter set used in this study produced an emission bandwidth from the USAF slide of about ~38 nm (500 nm – 538 nm) FWHM (Fig. 10 B-III) when directly measured with a spectrometer. We examined the effect of reducing the normal emission bandwidth by adding a longpass filter (521 nm cut-on) to obtain a 17 nm narrow emission bandwidth (Fig. 10 A-III). Finally we removed the 500 nm – 538 nm bandpass emission filter and used only the longpass filter and measured a fluorescence emission with a bandwidth of >50 nm and a greater than 50 nm tail of fluorescence (Fig. 10 C-III). As shown in column I, the images obtained using the SLM to create the diffractive imaging lens became markedly blurred with increasing bandwidth. However, as shown in column II, increasing the bandwidth of the fluorescence emission had little or no effect on the focus of the images obtained after reconstructing the holograms taken even with wide band fluorescence.
Fig. 10. Comparison of widefield and FINCH holographic imaging as a function of fluorescence emission bandwidth. The specimen was the USAF test pattern, imaged with an Olympus 20x 0.75 NA objective with a SLM-CCD distance of 400 mm. Columns I, II, and III respectively are widefield images, FINCH reconstructed images, and fluorescence emission spectra taken with varying emission filter combinations, as described in the text. Images and spectra in A, were taken with both a long pass and a standard emission bandpass filter, in B were taken with a standard emission bandpass filter and in C were taken with only a long pass filter. The FWHM fluorescence emission (in nm) was ~17 nm for the narrow bandwidth (Row A), ~38 nm for the normal bandwidth (row B) and >50 nm bandwidth with a > 50 nm tail (Row C) for the wide bandwidth emission fluorescence. The widefield images were obtained with input and output polarizers set at 0° with a 400 mm focal length diffractive lens pattern displayed on the SLM. The FINCH holograms were obtained with input and output polarizers set at 60° with an 800 mm focal length diffractive lens pattern displayed on the SLM. Best focus images were calculated from the holograms.

5. Discussion

By using the polarization properties of the SLM it is possible to utilize the same pixels to pass both the plane and spherical waves by including input and output polarizers in the system. This has two advantages: 1. The resolution of the lens patterns is increased because all of the SLM pixels can be used to more accurately represent the lens function (the quadratic phase pattern is not interrupted by non-functional pixels) 2. The plane and spherical wave come from the same pixel and thus the interference is not approximated from adjacent or otherwise random pixels. The configuration used in the present experiments was established to
determine the factors necessary for optimal resolution in a FINCH microscopy system. Thus the configuration is not the most light efficient. For example the devices used to control polarization are inefficient and reduce the light more than 50%. There is also only 25% efficiency by using the beam splitting cube so that the SLM can be used on axis. Having established the resolution potential of FINCH, it should be possible to produce diffractive lens patterns with the SLM positioned at 45°, eliminating the need for the beam splitter, so that most of the light is reflected into the camera and no light loss occurs at this step. Success in making this correction using wavefront analysis and Zernike corrections have been reported for SLMs [12]. Furthermore, more efficient polarizers can be used to reduce the light losses due to the use of polarizers.

In spite of the inefficiency of the light budget in our configuration, high quality reconstructed images were obtained at very low light levels. The signal to noise level in the FINCH system is not very dependent upon the intensity of the hologram being captured but is more dependent upon the extent of interference between the two waves propagating from the SLM. This is shown clearly in the matrix of images obtained from holograms captured at different polarizer settings in Figs. 8 and 9, along the diagonal with a constant ratio of \( \phi_1:\phi_2 \) (i.e. from (0,0) to (90,90)). The hologram in Fig. 8 at (0,0) is composed mostly of spherical wave from the SLM, while the hologram at (90,90) is composed mostly of plane wave. The corresponding reconstructed images in Fig. 9 both have extremely poor resolution, even though the holograms from which they are reconstructed are the brightest. The highest resolution reconstructed images in Fig. 9 derive from the holograms taken with the polarizers at intermediate angles, transmitting approximately equal amounts of plane and spherical wave. In contrast to what would be expected in conventional imaging, the highest resolution reconstructed images did not come from the holograms with the highest intensity, but rather from the holograms in which the greatest proportion of both plane and spherical waves produced the interference pattern. Thus, in FINCH imaging, obtaining a high degree of interference visibility between the couples of plane and spherical waves is a more critical factor than simply maximizing the intensity of the recorded holograms.

Another advantage shown here of our FINCH imaging configuration is its greater immunity to the wavelength dependent change in focal length of the diffractive lens. We observed the same sharp focus of images derived from FINCH holograms captured at narrow or very wide bandwidth. Under the same bandwidth conditions, when the SLM was used as a focusing lens and the bandwidth was increased as shown in Fig. 10, loss of focus occurred and blurring of the images was seen. In the case of regular imaging, changing the focal length \( f \) of an imaging lens leads to a change of the image distance \( d \) according to the imaging formula \( 1/d + 1/d_o = 1/f \); where \( d_o \) is the distance of object from the imaging lens. Therefore the transverse magnification \( M_T \) is also sensitive to the change of the focal length because of the relation \( M_T = d/d_o \). Consequently, for each wavelength there is a different image at a different location and with a different scale, which results in blurring of the overall image. This is not the case when the image being recorded is a FINCH hologram. As derived above from Eqs. (9) and (10), and for the case that \( z_e = f_o, f_o \to \infty \), we see that \( f_i = f_o/\lambda \) and \( z_r = z_o/\lambda \). Therefore \( z_r \) is sensitive to \( \lambda \) because of the dependence of \( f_o \) with \( \lambda \). However the transverse magnification \( M_T \) is independent of \( f_o \) and therefore it is independent of \( \lambda \). In other words, there is a different image for each wavelength, as in the case of regular imaging, but all the images appear in the same scale with FINCH imaging and are thus superimposed so that no blurring occurs due to chromatic diffraction effects.

Acknowledgments

We thank Barak Katz for sharing his results before publication and Dr. Brian Storrie and Dr. Edwin Heilweil for most helpful and continued advice and discussions. Supported in part by National Institutes of Health Grant 1 R43 EB008933-01A1 to GB, NISTARRA Award No. 60NANB10D008 to GB and BS and Celloptic, Inc.