Centrosome centering and decentering by microtubule network rearrangement

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ABSTRACT The centrosome is positioned at the cell center by pushing and pulling forces transmitted by microtubules (MTs). Centrosome decentering is often considered to result from asymmetric, cortical pulling forces exerted in particular by molecular motors on MTs and controlled by external cues affecting the cell cortex locally. Here we used numerical simulations to investigate the possibility that it could equally result from the redistribution of pushing forces due to a reorientation of MTs. We first showed that MT gliding along cell edges and pivoting around the centrosome regulate MT rearrangement and thereby direct the spatial distribution of pushing forces, whereas the number, dynamics, and stiffness of MTs determine the magnitude of these forces. By modulating these parameters, we identified different regimes, involving both pushing and pulling forces, characterized by robust centrosome centering, robust off-centering, or “reactive” positioning. In the last-named conditions, weak asymmetric cues can induce a misbalance of pushing and pulling forces, resulting in an abrupt transition from a centered to an off-centered position. Taken together, these results point to the central role played by the configuration of the MTs on the distribution of pushing forces that position the centrosome. We suggest that asymmetric external cues should not be seen as direct driver of centrosome decentering and cell polarization but instead as inducers of an effective reorganization of the MT network, fostering centrosome motion to the cell periphery.

INTRODUCTION In many cells, the centrosome is positioned at the geometric center of the cell, across a wide range of conditions: in cultured cells (Burakov et al., 2003), whether they have circular or elongated shapes (Hale et al., 2011) or symmetric or asymmetric adhesion patterns (Théry et al., 2006), in migrating cells (Gomes et al., 2005; Dupin et al., 2009), and in fertilized eggs (Wühr et al., 2010; Kimura and Kimura, 2011a; Minc et al., 2011). The robustness of this centering mechanism has been proposed to rely on the contribution of several types of mechanical forces acting on microtubules (MTs) by pushing and pulling on cytoplasmic organelles and cell borders, all contributing to stabilize the centrosome at the cell center (Zhu et al., 2010; Laan et al., 2012a). However, in vivo, the centrosome is mostly found at the cell periphery (Tang and Marshall, 2012). Indeed, in most differentiated cells, the centrosome is anchored to the plasma membrane, where it serves as a structural base for the primary cilium (Reiter et al., 2012). This simple consideration suggests that centrosome–MT networks not only have robust centering properties but also have efficient off-centering capacities. A global understanding of MT network geometry and centrosome positioning should therefore include the striking ability of this system to switch easily from a centering to an off-centering regime.

External cues are usually considered as the main driver of centrosome decentering. Indeed, centrosome displacement to the cell periphery can be triggered by an asymmetric cue such as contact with a neighboring cell (Rodriguez-Fraticelli et al., 2012) or a target...
cell (Yi et al., 2013). Such a cue generally induces local MT capture and the development of tension forces pulling the centrosome toward the cue (Combs et al., 2006; Kozlowski et al., 2007; Nguyen-Ngoc et al., 2007). However, for this mechanism to displace the centrosome up to the cell periphery, the decentering force associated with the asymmetric signal should overcome the centering forces. In such a scenario, cells would have difficulties in responding to minor changes in their environment.

Here we explore the possibility that the centrosome-MT network can adopt more “reactive” conformations in which centrosome position is stable but easily destabilized by a small change in MT organization. In such a state, the centrosome is the converging point of centering and decentering forces of comparable magnitude. Therefore a mild change in an intrinsic critical parameter or a small external cue can be sufficient to trigger network reorganization and thus bias the force balance so that decentering forces win over and move the centrosome to the periphery.

Minus end–directed motors, such as dynein molecules, produce pulling forces along MT length when bound to cytoplasmic vesicles or selectively on MTs tips when bound to the cell cortex (Kimura and Kimura, 2011b). The cytoplasmic localization of dyneins undoubtedly leads to a net centering force, since MTs that are longer on the side of the centrosome that is facing the more distant cell edge are pulled more strongly than MTs facing the closest cortex. The cytoplasmic pulling scenario also includes adherent cultivated mammalian cells with a flat (“fried egg”) geometry in which motors anchored on the basalf surface of the cell can pull microtubules all along their side. The contribution of dyneins anchored at the cell cortex is less clear. Cortical dyneins may have opposite effects on an isotropic radial array of MTs, depending on MT length distribution and dynein density relative to MTs (Laan et al., 2012b). MT pushing forces, generated by MT polymerization against the cell periphery, could also center or decenter the centrosome, depending on whether MT tips can slide or not on the cortex and affect the overall network symmetry (Holy et al., 1997; Tran et al., 2001; Faivre-Moskalenko and Dogterom, 2002; Brito et al., 2005; Pinot et al., 2009). The question of centrosome positioning has been explored with coarse-grained models (Théry et al., 2007; Zhu et al., 2010; Minc et al., 2011; Ma et al., 2014). With this approach, individual microtubules are not represented, and the force on the centrosomes is calculated as a sum of elementary forces calculated for each angular sector of the cell seen from the centrosome. This approach assumes that microtubules are straight and that the ones reaching the cortex do so in the line of sight from the centrosome. Typically, molecular motors are also not represented, and one assumes that their contribution results either in a constant force, in the case in which motors pull MTs at their tip, or in a force that is proportional to the distance between the centrosome and the cortex, for motors pulling MTs on their side. Pushing forces are assumed to act purely radially and often to be equal to the threshold for Euler-type buckling. Under these assumptions, the resulting equations can be analyzed simply. In other words, MTs are generally assumed to be no longer than the cell size, and their deformation is not considered to depart from a straight configuration. This condition might hold for early embryos or cells in a mitotic state, in which straight microtubules ensure the centering by pushing forces, and asymmetric distributions of cortical dyneins can induce the decentering (Grill et al., 2001; Garzon-Coral et al., 2016). In mammalian cells in interphase, however, MTs can be much longer and must bend to fit within the cell. This condition makes the coarse-grained approach impractical, but with modern computer hardware and state-of-the-art simulation methods, it is possible to consider every MT explicitly and solve the system correctly (Pinot et al., 2009; Maly and Maly, 2010; Wu et al., 2011).

To explore the balance between decentering and centering forces and tentatively reveal some relevant cellular parameters that would be interesting to focus on experimentally, we used numerical simulations. This approach allowed us to consider the effect of several factors that are likely to contribute to the regulation of force distribution. We examined microtubule bending and reorientation and basic parameters such as MT number, polymerization dynamics, and stiffness for their ability to break MT network symmetry. In this way, we identified the possible changes in network architecture that might misbalance pushing and pulling forces and promote centrosome decentering.

RESULTS

Centrosome positioning mechanisms are challenging to study because numerous factors such as cell shape, MT properties, or interacting proteins intervene and vary in different cell types and experimental conditions. Furthermore, there is currently no experimental way to measure the mechanical forces experienced by MTs in vivo, precluding the mapping of the spatial distribution of pushing and pulling forces that can be used for centering. Here we performed simulations with Cytosim software (Nedelec and Foethke, 2007). This cytoskeleton simulator is based on a Langevin dynamics approach and offers the possibility to take into account numerous components in minimal computational time due to a semi-implicit numerical integration scheme (Kozlowski et al., 2007; Loughlin et al., 2010, 2011; Ward et al., 2014).

We simulated pure centrosomal arrays in which all MTs are attached to a common center at their minus ends (Supplemental Figure S1). The angular distribution of MT nucleation is isotropic. We simulated systems containing one centrosome composed of 100 MTs for 400 s. MT growth followed the classical two-state dynamic instability model (see Table 1 and Material and Methods for numerical parameters). MTs were confined to regular geometries representing different idealized cell shapes. They could bend as linear elastic beams and thus follow Euler’s buckling theory. Entities that could bind/unbind and move along MTs were added to simulate the action of minus end–directed motors. Centrosome displacement is opposed by a viscous drag calculated to match the experimental observations. MTs growing against geometrical boundaries produced pushing forces, whereas minus end–directed motors generated the pulling forces (Supplemental Figure S1). By simply monitoring the position of the centrosomes, we could deduce whether the tested conditions resulted in a net centering or decentering effect.

Contribution of pulling forces

We first compared two scenarios in which motors such as dynein molecules are either distributed in the cytoplasm (Figure 1A and Supplemental Movie S1) or anchored at the cortex (Figure 1B and Supplemental Movie S1), in a situation in which MTs can be longer than the cell radius. In both cases, centrosomes moved toward the cell center regardless of the number of dyneins (except in the absence of motors; Figure 1C). Cortical distribution gave rise to a much faster centrosome motion (Figure 1C and Supplemental Figure S2). However, note that the simulations were done for an equal number of dyneins for both distributions, leading to highly different local densities: the higher number of cortical dyneins binding to MTs explained the difference in centrosome speed (Supplemental Figure S2).

To investigate further the effect of the cellular geometry on centrosome positioning, we switched to ellipsoidal, rectangular, and triangular geometries. We explored the two fundamental motor distributions by systematically varying the total number of motors in
the system to explore different ratios of motors to MTs. In the case of cytoplasmic localization of dyneins, the centrosome moved toward the center of gravity of the shape for any given initial position and all tested geometries (Figure 2A and Supplemental Movie S2), consistent with experimental observation in sea urchin eggs (Minc et al., 2011). In contrast, in the case of a cortical distribution, centrosomes did not move toward the center of gravity in the triangular geometries. After fast and erratic displacements throughout the cell, the centrosome usually converged toward the middle of the longest edge, which contains more dyneins (Figure 2, B and C, and Supplemental Movie S2). As in the circular geometry, switching to a cortical distribution led to stronger net forces, as illustrated by faster centrosome displacements (Figure 2C). These results showed how uneven angular distribution of cortical dyneins can act as a strong centering force, whereas for cytoplasmic dyneins, the net force was weaker and systematically directed toward the cell center.

### Contribution of pushing forces

MTs generate pushing forces as they polymerize against a barrier (Dogterom and Yurke, 1997). The spatial distribution of growing MTs within the cell affect the direction of the net pushing force exerted on the centrosome. If the aster is isotropic, pushing forces are directed toward the centrosome, but they are directed away from it in the case of anisotropic distribution (Pavin et al., 2012). Therefore any parameters influencing MT spatial distribution, such as nucleation, dynamics, or forces that induce bending, are likely to play key roles in determining the direction of the net pushing force on the centrosome. MTs are in particular easily deflected by forces applied on their ends. The net force on the centrosome will depend on MT stiffness, the number of MTs, and their configurations.

To investigate these effects, we considered a radial array of flexible MTs with their minus end anchored at the centrosome. MTs are anchored at regular angular intervals, such as to form an isotropic aster, but we tuned the angular stiffness of their anchorage to allow them to pivot at various degrees around their minus-end anchorage. In the basic setup, plus ends could glide along the edge of the cell, as the contact is considered to be frictionless, but by adding immobile anchors at the cortex that capture the plus ends and pin them, we can also prevent sliding. Thus varying the angular stiffness at the centrosomes and the strength of anchor points at the cortex enabled us to test the combinatorial effects of allowing or disabling minus-end pivoting and plus-end gliding (Figure 3A and Supplemental Movie S3). Initially, those simulations were performed in the absence of minus-end motor–associated pulling forces. As expected from MT

### TABLE 1: Default parameters used in the simulations.

| Parameter              | Description/reference                                      |
|------------------------|-----------------------------------------------------------|
| Microtubules           |                                                           |
| Ridity                 | $k_b T_{L_p} = 25 \text{pN/μm}^2$ Persistence $L_p = 5200 \text{μm}$ (Gittes et al., 1993) |
| Polymerization speed   | $V_0 = 0.13 \text{μm/s}$ Burakov et al. (2003)            |
| Depolymerization speed | $V_d = 0.27 \text{μm/s}$ Burakov et al. (2003)            |
| Rescue rate            | $0.064 \text{s}^{-1}$ Burakov et al. (2003)                |
| Stall force            | $f_s = 5 \text{pN}$ Dogterom and Yurke (1997)             |
| Catastrophe rates      | $0.01, 0.04 \text{s}^{-1}$ Unloaded catastrophe rate and stalled catastrophe rate; adapted from Janson et al. (2003); the unloaded rate is set higher than observed in vitro to take into account the absence of cytoplasmic obstacles |
| Total tubulin          | $M = 10,000 \text{μm}$ Total tubulin units available in the cell, expressed as length of MT |
| Centrosome             |                                                           |
| Radius                 | $0.5 \text{μm}$ Radius of centrosome bead                |
| Mobility               | $0.03 \text{μm/pN/min}$ From Zhu et al. (2010); in Cytosim, the mobility is calculated by setting an effective viscosity of 200 pN s/μm² for the bead around which the centrosome is built; this viscosity is only used calculate the mobility of the bead and does not affect the mobility of MTs |
| First anchoring stiffness | $k_s = 500 \text{pN/μm}$ Stiffness of first link anchoring MT minus ends to centrosome center |
| Second anchoring stiffness | $k_0 = 0$ or $500 \text{pN/μm}$ Stiffness of second link anchoring MT to a point on the centrosome periphery |
| Number of MTs          | 100 Zhu et al. (2010)                                    |
| Dyneins                |                                                           |
| Motion speed           | $V_{max} = 1.5 \text{μm/s}$ Unloaded speed toward the minus end of MTs (Gross et al., 2000) |
| Stall force            | $f_{sm} = 1.1 \text{pN}$ Stall force of a dynein motor (Gross et al., 2000) |
| Spring stiffness       | $k_d = 100 \text{pN/μm}$ Stiffness of the link between the dynein motor head and its fixed anchoring position |
| Confinement space      |                                                           |
| Cell radius            | 10 \text{μm} Radius for the basic circular geometry      |
| Confinement stiffness  | $k_c = 500 \text{pN/μm}$ Confinement strength of MTs inside the space |
| Pinning stiffness      | $k_g = 50 \text{pN/μm}$ Stiffness of the link that anchors MT plus ends to their contact point at the cell cortex, used to prevent gliding. |
observation in lymphoblast cell lines (Bornens et al., 1989) and previous numerical simulations (Pinot et al., 2009), when both pivoting and gliding were allowed, the network became asymmetric and pushed the centrosome off-center toward the closest edge (Figure 3A, top left). Indeed, MTs oriented toward the closest side were the first to reach the cortex and glide toward the opposite direction to minimize the bending energy associated with their curvature. This effect was reduced if MT pivoting was forbidden, as the aster remained more isotropic (Figure 3A, top right). Strikingly, when MTs gliding along the cell cortex was prevented, those first MTs in contact with the cell cortex were pinned and pushed on the centrosome, which was displaced toward the opposite cell edge (Figure 3A, bottom left). MT pivoting ability allowed them to join and form comet-like tail pushing the centrosome, as observed in Dictyostelium (Brito et al., 2005). Of interest, when both gliding and pivoting were prevented, the network never became asymmetric. Instead, it rotated briefly and adopted a vortex-shaped conformation in which the pushing forces kept the centrosome near the cell center (Figure 3A, bottom right). This centering effect by symmetric pushing forces was quite robust and independent of cell geometry (Supplemental Figure S3). As we reduced the strength of either the pivoting or the gliding stiffness while fixing the other, the network displayed rapid transition from centering to decentering (Figure 3C). This suggested that the modulation of these parameters can be an efficient way to break network symmetry and place the centrosome near the cell periphery (Figure 3, B and C). Of interest, these behaviors were independent of centrosome initial position (Figure 3B), meaning that if the centrosome is initially positioned at the cell center, the symmetry in the network will be spontaneously broken because of MT pivot, glide, or both, leading to centrosome decentering.

We then studied how MT stiffness, number, and length affected these behaviors. In the symmetric conformations of the network, when both MT gliding and pivoting were restricted, centering appeared robust with respect to a decrease in MT number and length (Supplemental Figure S4 and Supplemental Movie S5). The effects of changing MT stiffness were mild, between 20 and 100 pN/μm². Very soft MTs could not transmit polymerization forces efficiently, whereas very rigid MTs could not bend after reaching the cortex, in both cases freezing the centrosome motion (Supplemental Figure S4). If the MT network lost its isotropy, either because MT gliding along edges or pivoting around the base was allowed, then increasing the number of MTs progressively reinforced the net pushing forces and decentered the centrosome (Figure 4 and Supplemental Movie S4). We observed this effect by either raising the number of nucleation sites or decreasing the catastrophe rate. Increasing the stiffness of MTs also produced the same outcome. All of these parameters are therefore interesting targets if one wants to induce centrosome decentering.

Transitions from centering to decentering regimes

We then combined the pulling forces due to minus end-directed motors and the pushing forces due to MT polymerization to investigate the potential transition from centering to decentering regimes. Because dynein inhibition has been shown to induce centrosome decentering (Burakov et al., 2003; Wu et al., 2011), we assumed that dynein-associated forces contributed to center the centrosome, that is, that dynein molecules are anchored in the cytoplasm rather than at the cell cortex. We first wanted to know whether a centrosome could spontaneously move off center in the absence of asymmetric cues. We thus tested whether a global variation of the MT network properties, such as the parameters described here, could overcome the centering effect of cytoplasmic dyneins and promote centrosome displacement to a peripheral position.

As found in the first part of this study, with a high concentration of cytoplasmic dyneins (4000 dyneins per cell, corresponding to 40 per MT), MT outward-pushing forces were not sufficient to overcome the dynein-induced centering effect (Figures 1 and 2). Transitions were seen only in cells in which the dynein concentration was reduced. In the following simulations, we used 100 dyneins per cell (i.e., 1 per MT). This condition is physiologically relevant because it has been shown that pushing and pulling forces are of comparable magnitude (Zhu et al., 2010). We thus studied the conditions in which variations in MT rigidity, number, and catastrophe rate, as well

![A Cytoplasmic dyneins](image1.png)  
![B Cortical dyneins](image2.png)  
![C Cytoplasmic](image3.png)  

**FIGURE 1:** Centrosome centering by pulling forces. (A) Simulation in which the motors are distributed in the cell. (B) Simulation in which the motors are distributed only on the edge the cell. Dynein motors are shown in green and MTs in black. Right, centrosome positions, indicated by colored points, from blue (0 s) to red (400 s). Left, centrosome trajectories. The gray area is the area filled by motors. (C) Variation of the number of motors for both cytoplasmic and cortical motor distribution. Fifteen trajectories are shown on each plot, in which the number of simulated dyneins is increased from 0 to 7000 with a step of 500. The initial position of the centrosomes was set on an arc axis to make them all visible on a single plot. This should not affect the outcome of the simulation, since the system has rotational symmetry. In all cases, the centrosomes are initially placed at a distance from the center corresponding to half the cell radius. Right, maximal speed reached by the centrosome during each simulation as a function of the number of dyneins for both cortical and cytoplasmic distributions. Each symbol is the result of one simulation, and the lines are guides for the eye.
The pushing forces are stronger (because they scale as $1/L^2$ according to Euler’s theory; Figure 5, B and C, and Supplemental Movie S6). Reducing drastically the catastrophe rate turned the centering regime into a weak decentering one (Figure 5B). The system was quite sensitive to the number of MTs, and a progressive transition from centering to decentering occurred as the number of MTs increased (Figure 5C). Varying either centrosome angular stiffness (which affected pivoting) or cortex anchor stiffness (which affected sliding) had even more drastic effects and could induce abrupt transitions in the position of the centrosome (Figure 5, D and E, and Supplemental Movie S6). From these results, the ability of the network to reorganize asymmetrically appears as a key regulator of the force balance at the centrosome.

Of note, these results showed that moderate changes in any of the tested parameters, isolated or in parallel, were often sufficient to induce a complete reversal of whether the centrosome is located at the center or near the periphery of the cell. In the case in which the transition is not complete, a parameter change could prime the network for such a transition. For example, allowing the network to be asymmetric increased the net force on the centrosome. Even when this force was effectively balanced by the inward-pulling forces exerted by cytoplasmic dynein, it made the reversal more likely to occur if another perturbation was added. For example, the net inward-pulling force can be further reduced by additional asymmetric outward-pulling forces, such as those exerted along cell–cell contacts. This idea was tested by adding external cues, which were simulated by adding cortical dyneins within a 60°-wide crescent. We then compared the response of a “constrained” network, in which MT central pivoting and peripheral gliding were forbidden, and the response of a “reconfigurable” network in which pivoting and gliding are allowed, to increasing amounts of localized cortical dyneins (Figure 6A). The constrained network was less sensitive to asymmetric pulling forces, since the pushing from the captured MTs opposed the tension developed by the cortical dyneins (Figure 6A and Supplemental Movie S7). By contrast, the reorientation of MTs in the “reconfigurable” network redirected some polymerization forces toward the cortical pulling site (Figure 6B and Supplemental Movie S7). Thus the “reconfigurable” network appeared more responsive to external cues, and the centrosome decentered more readily (Figure 6C). Together these results indicate that several intrinsic parameters of the MT networks, such as MT number, rigidity, and in particular the ability to reorient MTs, is key to modulating the response of the cell. The magnitude and distribution of pushing forces could either lead to robust centering of the centrosome or place it in a reactive conformation.
where it could respond to weaker external asymmetric stimulation. Such reactive conformations are characterized by spontaneous symmetry-breaking events and centrosome decentering in the absence of asymmetric external cues.

**DISCUSSION**

The process of centrosome positioning is still under investigation, in particular because different mechanisms can prevail in different cellular conditions (Ma et al., 2014). Here we focused on conditions in which MTs can be longer than the cell diameter, which is the case for adult mammalian cells in interphase (Wu et al., 2011), rather than the more usually studied large mitotic cells in embryos (Kimura and Onami, 2007; Wühr et al., 2010; Minc et al., 2011). Under these conditions, several parameters could regulate the symmetry of MT network architecture, independently of external cues or preexisting asymmetries in boundary conditions such as local capture, stabilization, or mechanical forces. MT number, length, and rigidity, as well as centrosome stiffness, all have the ability to induce a spontaneous network symmetry break and thus lead to centrosome decentering.

Centering capacities are generally considered to result from minus end–directed motors such as dyneins (Kimura and Kimura, 2011b). Here, by using numerical simulations, we compared the contributions of cytoplasmic and cortical dyneins. We confirmed that cytoplasmic dynein molecules induce robust centrosome centering, whereas cortically anchored dyneins are capable of promoting either centering or decentering, depending on cell shape (Ma et al., 2014). Asymmetric pulling forces due to cell shape extension promoted centrosome decentering toward the longest cell edge.

Next we studied how the MT network configuration determined the orientations of pushing forces associated with MT polymerization. When MTs are tightly constrained in space, that is, if they cannot pivot around their anchor point in the centrosome and if their plus ends cannot glide along the cell edge, they maintain an isotropic distribution and generate centering forces. In contrast, when the MTs are free to pivot or slide, the net pushing force pushes the centrosome toward the periphery. In both scenarios, MT stiffness and number can modulate the speed at which the centrosome moves. Thus, when pushing forces are opposed by dynein-induced pulling forces, modifying the number of MTs or their stiffness could trigger a transition from a regime in which the centrosome is at the center to a regime in which the centrosome adopts a peripheral position.

We investigated some theoretical mechanisms that can affect MT architecture and centrosome positioning, limiting our approach to numerical experiments. The results pointed to the possible role of several parameters, suggesting possible experimental investigations.

Centrosome angular anchor stiffness appeared as a critical parameter, since small variations from 20 to 5 pN/μm were sufficient to induce an abrupt transition from a centering to a decentering regime (Figure 5E). The anchoring of MTs at the centrosome is not well characterized. MTs can detach from the centrosome in mammalian cells (Keating and Borisy, 1999; Alieva et al., 2015) and were seen to pivot around yeast mitotic spindle poles (Kalinina et al., 2012), but the angular stiffness has not been measured. The pivoting of a MT with respect to the centrosome is likely to depend primarily on the stiffness of the pericentriolar material in which MTs are embedded. Regulation of pericentriolar material density and cross-linking density (Woodruff et al., 2014), as well as the polymerization of actin filaments nearby (Farina et al., 2016), could possibly affect this stiffness. Moreover, the ability of MTs under tension to tear apart pieces of pericentriolar material during specific phases of the cell cycle suggests that the material stiffness is precisely regulated (Megraw et al., 2002; Rusan and Wadsworth, 2005; Krueger et al., 2010).

Pushing forces naturally scale in proportion with the number of MTs in the aster and inversely with the squared length of the MT, but these parameters also have a less obvious effect on the network symmetry (Figure 4). They vary widely from one cell type to another and also during cell cycle progression (Piehl et al., 2004). It would be interesting to look at them in more detail during centering-to-decentering transitions—for instance, during epithelial morphogenesis, ciliogenesis, or immune synapse formation.
Our simulations confirmed a strong role for MT stiffness, which was expected since MT bending stiffness is a key parameter in the transmission of MT polymerization force produced at the plus ends to the centrosome attached at the minus ends and thereby regulates the net force on the centrosome. Increasing the MT stiffness is sufficient to switch from a centering to a decentering regime (Figure 5A). Several parameters have been shown to affect MT rigidity (Hawkins et al., 2010). MT-associated proteins can either increase (Felgner et al., 1997) or decrease (Portran et al., 2013) MT bending stiffness. MT cross-linking molecules can also modulate the size of MT bundles and consequently their rigidity (Bathe et al., 2008) and thus affect the system similarly.

Cortical stiffness in our simulations reflects the interaction that MTs have with the cell cortex and is a property of the cell cortex. MT ability to glide or not along cell cortex was key to network rearrangement, symmetry breaking, and the orientation of pushing forces toward the cell periphery (Figures 3 and 5D). This parameter reflects the fact that MTs could get entangled in a crowded cortical actin network or be physically linked to those microfilaments (Coles and Bradke, 2015). Plus ends have been seen to grow or not along the cell periphery, depending on the presence of filament bundles or branched meshwork, suggesting that the local actin architecture could regulate MT gliding (Thény et al., 2006). Accordingly, changes in cell adhesion and modifications of the associated cortical actin network could result in MT network rearrangement and induce centrosome repositioning.

For the sake of simplicity, several factors were not taken into account in our simulations, notably the contribution of noncentrosomal MTs (Alieva et al., 2015) and kinesins (Cross and McAinsh, 2014), although we know that these factors contribute to the intrinsic regulation of force production and network reorganization. We also ignored key external contributions, such as centrosome and MT interactions with the nucleus (Burakov and Nadezhdina, 2013) and the production of forces by the actin cytoskeleton (Waterman-Storer and Salmon, 1997; Gupton et al., 2002). Also of importance, we considered that the cytoplasm was devoid of obstacles and that MT motions were hindered only by cell boundaries. The elasticity of the actin network and other obstacles surrounding MTs might, however, constrain their deformation and significantly increase the magnitude of pushing forces transmitted to the centrosome (Brangwynne et al., 2006; Shan et al., 2012). These important parameters deserve further investigation.

In this work, we studied the ability of MT asters to become anisotropic, a reorganization of the MT network that ultimately pushed the centrosome near the cell periphery. In physiological conditions, the MT cytoskeleton within a cell is rarely isolated, as cells contact other cells. These contacts represent external cues that affect the MT network within each cell. A MT network spanning the entire cytoplasm can physically integrate all these contributions from the surrounding tissue. Ultimately, the position of the centrosome thus results from the spatial integration of all of the peripheral cues, either filtered or amplified, depending on the intrinsic properties of the MT network.

**MATERIALS AND METHODS**

All simulations were performed using Cytosim (www.cytosim.org). The values of the main parameters are presented in Table 1. The motion of elastic fibers surrounded by a viscous fluid (we used a viscosity of 1 pN s/μm²; Kole et al., 2005) was calculated using Langevin dynamics (Nedelec and Foethke, 2007). Microtubules were thus subject to Brownian motion as determined by their size and temperature (k_BT = 4.2 pN·nm).

**Microtubule dynamics**

MT minus ends are stably anchored to the centrosome. Plus ends undergo dynamic instability (Mitchison and Kirschner, 1984) following a two-state model. Each state is implemented in Cytosim as:

- Polymerization occurs with a speed \( V_g \) that is proportional to the free tubulin pool in the cell and decreases exponentially under opposing force as measured (Dogterom and Yurke, 1997):

\[
V_g = V_0 \frac{\alpha \exp(-f / f_c)}
\]
where $f$ is the force component parallel to the axis of the MT, $f_s$ is the stall force, $V_0$ is the growth speed parameter, and $\alpha$ is a dimensionless factor of range $[0, 1]$ representing the fraction of monomer available in the cell. This factor is calculated from the sum of all MT lengths in the cell divided by the total available tubulin pool, expressed in units of MT length:

$$\alpha = 1 - \frac{1}{M} \sum L_i$$

- Depolymerization occurs at a constant speed, $V_d$.
- Catastrophe events occur with a rate, $\tau_c$, that depends on the growth speed of the fiber:

$$\tau_c = \tau_{\text{stall}} \left(1 + \frac{\tau_{\text{stall}} - 1}{\tau_0} \frac{V_0}{V_0}\right)$$

where $\tau_{\text{stall}}$ is the rate of catastrophe of a stalled microtubules, which is greater than the rate of catastrophe of a free microtubule, $\tau_0$ (Janson et al., 2003).

- Rescue events occur at a constant rate, $\tau_r$.

Microtubule bending elasticity

Microtubules are modeled as semiflexible polymers (Nedelec and Foethke, 2007), and their buckling thus follows Euler’s law. If the loading is slow, buckling occurs in the first mode, at a threshold of force given by, for a length $L$ and a persistence length $L_p$,

$$f_k = \pi^2 k_a T L_p L^2$$

Centrosome

The centrosome is simulated as an aster with a fixed number of microtubules. All MTs are attached to a small bead of radius $R$ whose mobility (i.e., inverse of the drag coefficient) is chosen to match the value of the mobility calculated for the centrosome in Zhu et al. (2010) to take into account centrosome motion velocities experimentally measured in Burakov et al. (2003). The microtubules are anchored at the center of the aster with two Hookean links. The first link, of stiffness $k_a$, attaches the minus end of the MT with the center of the bead. The second link, of stiffness $k_b$, attaches a distal point on the surface of the bead with the point of the MT that is located at distance $R$ from the minus end. The number of distal points on the bead is equal to the number of MTs in the

\[\text{FIGURE 5: Transitions between centering and decentering regimes. (A–E) Simulations in which one parameter was geometrically varied: MT rigidity, from 1 to 260 pN/\mu m^2; MT unloaded catastrophe rate, from 0.01–0.06 s}^{-1}; \text{number of MTs, from 15 to 350; MT gliding stiffness while pivoting is not allowed, from 0 to 10 pN/\mu m; and MT pivoting stiffness when gliding is not allowed, from 0 to 110 pN/\mu m. In each case, 100 cytoplasmic dynein motors were randomly positioned in the cell and one parameter of the system was varied systematically. Cell radius is 10 \mu m in A and 7 \mu m in B–E. Left, exemplary simulations for two different outcomes observed while varying a parameter. Middle, trajectories of simulations obtained while varying a parameter, displayed along an arc, with values increasing from left to right. For each trajectory, time is indicated by the color, from blue (0 s) to red (400 s). The center of each disk is marked with a black dot. Right, centrosome positioning as a function of various parameters, measured by the distance to the cell center. The dotted line represents the initial centrosome–center distance (half of the confinement radius). In A–C, MTs were allowed to pivot and glide.}\]
a force that is always orthogonal to the edge, thus corresponding to a perfectly slippery edge on which MTs can slide freely. However, in some simulations, the plus end of a MT reaching the edge of the geometry was “pinned” by a spring of stiffness \( k_{\text{g}} \) acting between the microtubule plus end and the point at which the plus end first reached the edge. When this constraint is added, gliding of microtubules along the cortex is strongly impaired, and the impediment depends on \( k_{\text{g}} \). It is interesting to note that we chose to implement cortical friction as a pinning system rather than a local friction term for simplicity. Both friction modes could be envisaged, as they might depend on cell conditions, as noted in the Discussion (adherent or nonadherent cells, cell in tissue or isolated, cell wall presence or not, etc.). It would be interesting to compare the effects of both frictional constraints in future studies.

Motors

A dynein molecule is simulated as a point-like object that can bind and unbind to microtubules linked to a fixed position by a spring of stiffness \( k_d \). This spring represents the anchorage of dyneins either at the cortex or on some vesicle in the cytoplasm. The dynein head moves on a fiber with a speed that depends on the load experienced by the spring:

\[
V = V_{\text{max}} \left( 1 - \frac{f}{f_{\text{stall}}} \right)
\]

where \( V_{\text{max}} \) is the speed of a motor without load and \( f_{\text{stall}} \) is the motor stall force. The value of \( V_{\text{max}} \) used here is negative, representing the fact that the dynein head moves toward the minus end of the microtubule.

Strong cortical motors

Strong cortical motors were added to the simulation to represent the possible effect of local motors associated with proteins such as Par3 in the cortical environment. The particularity of these motors is that they do not unbind unless the microtubule is shrinking. Moreover, these motors stabilize MTs. Specifically, when one or more motors is bound within 0.5 \( \mu \text{m} \) of a plus end, the catastrophe rate of this MT plus end is temporarily set to zero, such that it continues to grow. The other parameters describing the motor (speed, stall force, spring stiffness, etc.) are kept equal to those of classic motors.

Analysis

Analysis graphics were generated with open source R software. The general tendency of distance to center evolution was fitted with a spline curve of degree four to six according to the smoothness of the data (using the smooth.spline R function) and is shown as a solid black line in the graphics.
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