Introduction

It is well acknowledged that the auditory brainstem response (ABR) test is regarded as an objective test through the auditory peripheral pathway to a central level of the brainstem, and usually evaluates the hearing sensitivity and diagnoses the types of hearing loss and neurological disorders [1,2]. Many clinicians have used ABR of especially air-conduction (AC) for patients who might suspect those pathologies. As a result, AC ABR test has been a useful for obtaining clinical outcomes while also providing absolute values of latency and amplitude from ABR waves.

Nevertheless, there are some limitations to AC ABR in the following specific situations: 1) patients who have multiple disorders that could be attributed to cognitive ability or behavioral self-control [3], 2) populations that have conductive hearing loss such as external auditory canal atresia (EACA), aural atresia, and microtia [4]. The most common cause of failing to obtain AC ABR thresholds in infants is due to conductive deafness [5]. In other words, children and adults who could check behavioral hearing thresholds through both air- and bone-conduction pathways might be conducted by only AC ABR in general and also assumed any possible conductive problem. However, this is not a simple approach for infants who have undergone diagnostic ABR testing, especially for those who have failed multiple neonatal hearing screening tests that have only examined the AC pathway (i.e., from the
ABR records. The vibrator to head coupling method reported in previous investigations has demonstrated consistent results with ABRs to BC clicks in infants [7,8,15]. Currently, specific techniques and results for BC ABR have been well documented by the British Columbia Early Hearing Program [10] (please visit this reference).

**Placements for Bone Oscillator**

While conducting BC ABR tests, many clinicians have experienced large amounts of artifacts. This is true, especially at high intensities with 50 dB above normal hearing level (nHL) and also at earlier waves such as Wave I. To avoid stimulus artifacts, the bone oscillator should be placed high on the temporal bone, and the inverting electrode should be placed on the earlobe, mastoid, or nape of the neck. Artifacts could also be reduced with an alternating phase stimuli. Since the output of most bone oscillators is around 45 to 55 dB nHL, it becomes difficult to distinguish between sensorineural or mixed hearing losses when the losses by bone exceed this range. This output limitation of the bone oscillator is a drawback.

A previous study that examined different oscillator placements for BC ABR reported that the wave V affects the placement of the oscillators in infants, although adults were less affected by the bone vibrator. In addition, infants showed a delayed latency of wave V in the occipital and frontal lobe than in the temporal lobe for both AC and BC ABR [8]. Stuart, et al. [7] reported on BC ABR for three different placements in temporal bone and found that the posterior and supero-posterior placements could generate clearer waveforms with shortened latency than in the superior placement. De Freitas, et al. [16] reported that oscillator placement on the mastoid could estimate a lower level of thresholds than on the forehead. The density and thickness of the cranial bones and fontanelles, which comprises any soft membranous gap between the cranial bones that make up the calvaria of a fetus or an infant, are factors that can affect oscillator placement for BC ABR in adults and infants [7,8]. Table 1 provides useful information for determining the bone oscillator placement for clinical application.

**Stimuli for Bone-Conduction ABR**

Since brief click stimuli have no frequency specificity, clinicians are unaware of which frequencies particularly contribute to the click limit during testing. In this regard, tone stimulation would be useful to obtain frequency-specific thresholds. Although click ABR thresholds are known to be insufficient, we currently still use broadband click stimuli for many clinical
ABR thresholds. Rather, tone-evoked ABR tests have been used successfully in both research and clinical settings [1]. In particular, tone-evoked ABR for BC stimulation has been used for at least 20 years for research and clinical purposes. For example, Stapells and Ruben [6] investigated BC ABR using 500 and 2,000 Hz tones for forty-eight infants (mean age: 6.1 months) with either normal hearing (24 ears) or conductive hearing loss (41 ears). They suggested that clinically nHLs could be attained at ABR thresholds to BC stimuli of 30 dB nHL for 2000 Hz and 20 dB nHL for 500 Hz.

Unfortunately, although reference equivalent threshold sound pressure levels have been provided for click and tone-pip stimuli used for AC ABR by ISO 389-6 since 2007, there is no standard reference equivalent force threshold levels for tone-pip stimuli of BC ABR yet, but only for click BC ABR. Furthermore, there are few published reports on tone-evoked BC ABR for patients with hearing loss. Vander Werff, et al. [18] did not find meaningful thresholds of BC ABR from infants with sensorineural hearing loss due to a very small study size (n is 2 for 500 Hz and n=9 for 2,000 Hz). More recently, Hatton, et al. [5] successfully obtained thresholds with 98% accuracy in 500 and 2,000 Hz BC tone stimuli to differentiate children with conductive and sensorineural hearing loss. Table 2 shows the measurement parameters for various stimuli that have clinical utility.

Table 1. Summary of bone oscillator placement for bone-conduction auditory brainstem responses recommended by several studies

| Subjects         | Yang, et al. [8] | Yang and Stuart [15] | Stuart, et al. [7] | De Freitas, et al. [16] |
|------------------|------------------|----------------------|--------------------|------------------------|
| Age (years)      | Neonates 0–4 m   | 1-year-old infants   | 38–42 weeks        | 20–30 years            |
| Adults           |                  |                      |                    |                        |
| Number           | 10 individuals of each group | 48 | 25 | 22 |
| Hearing condition| Normal           | At-risk for hearing loss | Normal           | Normal                |
| Consideration factors | Radioear B-70A vibrator | Radioear B-70B vibrator | Radioear B-70B vibrator | Radioear B-70B vibrator |
| Placement        | Temporal bone    | Supero-posterior auricular position | Supero-posterior of temporal bone | Mastoid |

Table 2. Summary of measurement parameters for bone-conduction auditory brainstem responses recommended by several studies

| Stimuli                        | Foxe and Stapells [17] | Hall [9] | Hatton, et al. [5] | De Freitas, et al. [16] |
|--------------------------------|------------------------|----------|--------------------|------------------------|
| Filter (Hz)                    | 30–3,000               | 30–3,000 | 30–1,500           | 30–3,000               |
| Array                          | C2-M1/M2               | Fz-M1/M2 | Fz-M1/M2           | Fz-A1/A2               |
| Polarity                       | Alternating            | Alternating | Alternating      | Alternating            |
| Rate (/sec)                    | 39.1                   | 7.1      | 39.1               | 27.7                   |
| Sweeps                         | 2,000                  | More than 2,000 | 2,000              | 2,000                  |

Threshold of Bone-Conduction ABR

By presenting stimuli to the BC pathway, BC ABR is able to perceive hearing loss and neural disorders for patients with limited AC ABR or behavioral (i.e., pure-tone audiometry) testing. This characteristic of BC ABR allows it to be utilized not only for patients who have low reliable AC ABR outcomes due to diseases of the AC pathway but also infants and toddlers [3]. Moreover, there are many features of BC ABR. As mentioned earlier, while AC ABR transmits stimuli using head-phones or earphones through the AC pathway, BC ABR presents stimuli with the oscillator through the temporal bone directly to the cochlea [8]. The vibration of the temporal bone and cochlea generates binaural attenuation caused by signal dispersion in the cranial bone.

This difference between AC and BC ABR manifests in the latency of wave V. The wave V latency of BC ABR was approximately 0.5 ms longer with a larger amplitude than AC ABR [19]. The amplitude of wave V and early waveform modalities seem to change with the level of the stimuli. For high level stimuli, BC ABR was not differentiated from AC ABR for the amplitude of wave V and early waveforms. In contrast, with low level stimuli (under 55 dB nHL), the latency of wave V was delayed approximately 0.5 ms compared to AC ABR, and the early waveforms were not clearly distinguished. A previous study that compared both infant and adult AC and BC ABR thresholds found that the latency of wave V was delayed approximately 0.5 ms in BC ABR compared to AC ABR.
ABRs reported that infants showed similar thresholds for both ABR tests (3.75 and 1.25 dB nHL, respectively), whereas adults showed a significant difference between AC and BC ABR thresholds (3.75 and 18.75 dB nHL, respectively).

### Latency of Bone-Conduction ABR

BC ABR waves typically appear more rounded than more conventional AC ABR. The maximum output of 50 dB nHL stimulated by the bone oscillator should appear similar to the 50 dB nHL response of AC for people with normal hearing or with a mild sensorineural hearing loss. If a patient has conductive hearing loss, the latencies for AC are shifted when compared to the latencies of BC ABR.

### Comparison with AC

Several studies have found that the latencies of the ABR waves to BC stimuli are approximately 0.16 to 0.88 ms longer than those to AC stimuli [8,19]. Such a latency discrepancy has been thought to be due to the low pass filter characteristics of the bone vibrator. In other words, BC stimuli would excite more apical cochlear regions with a longer traveling wave delay than the corresponding AC stimuli [8,19]. Durrant and Hyre [20] had suggested that this delayed BC response may be related to the propagation delay and low pass filtering involved in skull vibration. Gorga, et al. [21] have also explained that there may be some inherent differences in the transmission of energy between AC and BC stimuli.

### Age effect

As stated previously, the wave V latencies derived from BC ABR are approximately 0.5 mms longer than those from a same intensity of AC stimulus. For infants, the wave V latencies evoked by BC clicks are shorter than those of AC clicks [8]. Many researchers have insisted that these differences can be explained by the changes of skull due to aging.

### Gender effect

In general, the studies documenting gender differences in the AC ABR have reported shorter absolute wave latencies and larger wave amplitudes for female participants. To examine the gender differences of infants, Stuart and Yang [22] measured wave V latency thresholds of two hundred and two full-term neonates (103 males and 99 female) using AC and BC click stimuli of 30, 45, and 60 dB nHL and 15 and 30 dB nHL, respectively. The results demonstrated that female newborns showed significant shorter wave V latencies than male newborns for AC click stimuli (i.e., approximately 0.2–0.3 ms). However, there was no significant gender difference in wave V latencies when applying click stimuli for BC ABR.

### Clinical Outcomes

#### Maturation: infants and young children with normal hearing to adults

BC ABR can estimate cochlear function in infants and help identify any types of hearing loss that could be present [6,8,15,23]. Hooks and Weber [23] studied BC ABR stimulated by clicks in premature infants and showed that there were large differences in ABR results between infants and adults in terms of morphology, latency, and amplitude. These differences are thought to be caused by the maturation of the auditory pathway in infant. The morphology, latency, and amplitude of infants’ ABR results showed similar characteristics as adults. Full-term infants showed the wave I, III, V, and a delayed inter-wave and absolute latency compared to adults [24]. Their latency of wave I becomes adult-like by six to twenty-four weeks, and waves III and V become adult-like by 18 months of chronological age [24]. BC ABR showed more delayed latency than AC ABR, in general.

### Pathology: congenital EACA

As mentioned previously, infants showing elevated ABR thresholds to AC stimuli should be further tested with BC stimuli. Infants with atresia, microtia, otitis media, and other
Patients with congenital hearing aural atresia predominantly exhibit a lack of inertia in the ear chains. For example, Chen, et al. [4] compared the differences in AC and BC ABR latency for children with congenital EACA and normal hearing. Although the EACA group demonstrated significantly higher (i.e., worse) AC ABR thresholds due to the pathology in the AC pathway, there were no significant differences in BC ABR and BC ABR latency between groups. These findings demonstrate that BC ABR had clinical utility for the examination of cochlear, auditory nerve, and central auditory pathway function. Table 3 provides the recommended absolute latencies of waves I, III, and V conducted by BC ABR for both infants and adults who structurally and functionally had normal hearing, and infants with atresia. The absolute latencies will be helpful for utilizing BC ABR in the clinical setting.

### Bone-Conduction ABR Applications for Bone-Conduction Hearing Implants

In case of clinical purpose, ABR assessed to estimate thresholds and to classify types of hearing losses. The Joint Committee on Infant Hearing (2007), National Institutes of Health (1993) and American Speech-Language-Hearing Association (2004) all support the use of ABR for universal newborn hearing screening. BC ABR can be used to specifically identify the different types of hearing losses. However, the patients usually limit for infants and not apply routinely. Importantly, BC ABR could be an alternative to AC ABR in patients with diseases of the AC pathway. BC ABR showed larger amplitudes of wave V and clearer waveforms for patients with atresia or microtia. These advantages of BC ABR could be applied for bone anchored hearing aid (BAHA) utility and offer definite testing results. In conclusion, overall comparison and understanding of BC pure-tone audiometry, BC ABR, and results by oscillators using BAHA may lead to scientific evidence for mapping BAHA and expect accurate performance of BAHA users.

Recently, BAHAs have been placed in patients with conductive hearing loss or congenital atresia. In 2001, Setou, et al. [28] revealed the existence of a BC-binaural interaction component (BIC) in normal hearing adults and suggested that the bilateral fitting of BC hearing aids in children with atresia allow for the localization of the sound. Since then, many studies have also reported that BC-BIC is present in children with congenital atresia as well as normal-hearing adults, and the gross response properties of BIC are similar between these two populations. Such a BAHA system has several clinical applications and has proved to be reliable. In some cases, it is necessary to estimate aided and unaided pure-tone audiograms by objective methods, especially for passively cooperative subjects like young children; to this end, Eggermont has developed a stimulated one. Electroencephalography receives typical changes with time correlation and sound stimulation [17]. ABR appears as a series of vertex positive waves occurring within 15 ms of the start of transient stimulation. An auditory evoked potential (AEP) measurement using BAHA has been reported for patients with unilateral sensorineural hearing loss [29]. A free field sound stimulus with a sound intensity level of 80 dB HL, requires masking or occlusion of healthy ears, was used in this study. According to Rahne, et al. [30], recording ABR and AEP by delivering a stimulus via BAHA yields a response waveform comparable to the response waveform induced by earphone stimulation. They suggested that the thresholds of ABR and AEP seem to match the subject’s normal hearing.

### Conclusion

In the clinical setting, ABR audiometry has been used as a powerful objective tool to evaluate hearing sensitivity and to diagnose various types of hearing loss and neurological disorders. Although BC ABR could be an alternative to AC ABR...
as it overcomes some limitations of the latter, the majority of clinicians rarely use it due to a lack of knowledge and no routine test administration. Based on several clinical BC ABR protocol guidelines mentioned in this review, a comparison between AC and BC ABR should be applied to characterize the degree of hearing loss and to differentiate its types. Moreover, BC ABR can be helpful in determining subsequent test timing, and can be important for both appropriate follow up and parent counselling.

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Conflicts of interest
The authors have no financial conflicts of interest.

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