Research Article

Effect of Heat and Mass Transfer and Magnetic Field on Peristaltic Flow of a Fractional Maxwell Fluid in a Tube

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Magnetic field and the fractional Maxwell fluids’ impacts on peristaltic flows within a circular cylinder tube with heat and mass transfer were evaluated while assuming that they are preset with a low Reynolds number and a long wavelength. The analytical solution was deduced for temperature, concentration, axial velocity, tangential stress, and coefficient of heat transfer. Many emerging parameters and their effects on the aspects of the flow were illustrated, and the outcomes were expressed via graphs. Finally, some graphical presentations were made to assess the impacts of various parameters in a peristaltic motion of the fractional fluid in a tube of different nature. The present investigation is essential in many medical applications, such as the description of the gastric juice movement of the small intestine in inserting an endoscope.

1. Introduction

Numerous implementations have drawn interest of physicists, mathematicians, and engineers on magneto-hydrodynamic flow issues. In some applications and geothermal studies, metal alloy substantiation processes are optimized Sources, management of waste fuel, regulation of underground propagation and pollution of chemicals, waste, the construction of energy turbines for MHD, magnetic equipment for wound therapy and cancer tumour treatment, reduction of bleeding during surgery and transport of targeted magnetic particles as medicines. Several extensive works of literature on that fertile field are now available in [1, 2]. Saqib et al. [3] clarified the nonlinear motion of the non-Newtonian fractional model fluid problem. Rashed and Ahmed [4] produced a numerical solution for dusty nanofluids peristaltic motion in a channel using a shooting method. The slip effect’s problem on a peristaltic flow of the fractional fluid of second-grade over a cylindrical tube was examined by Rathod and Tuljappa [5]. Vajravelu et al. [6] obtained the velocity, temperature, and concentration with a magnetic field of a Carreau fluid in a channel with the heat and mass transfer. Ali et al. [7] discussed magnetic field effects on a blood flow that the blood was characterized as the Casson fluid. Zhao et al. [8] explored the motion natural convection temperature of a fraction with a magnetic field of viscoelastic fluid through a porous medium. Abd-Alla et al. [9] were researching the magnetic field’s impact on a peristaltic motion of the fluid through the cylindrical cavity. Afzal et al. [10] analyzed the effect of the diffusivity convection and magnetic field in nanofluids on the peristaltic motion through the nonuniform channel. Heat and mass transfer’s effects and magnetic field of the peristaltic motion in a planar channel were examined by Hayat and Hina [11]. The impact of the temperature and the magnetic field of peristaltic motion through a porous medium was debated by Srinivas and Kothandapani [12]. Ramzan et al. [13] discussed the heat flux and magnetic field’s influences in Maxwell fluid flow through a two-way strained surface. Rachid [14] calculated the movement of viscoelastic fluid peristaltic transport under the Maxwell fractional model. The impact of a viscosity and a magnetic field of the peristaltic motion of synovial nanofluid in an asymmetric channel was reconfirmed by Ibrahim et al. [15]. Aly and Ebaid [16] inspected the slip conditions’ effects of a peristaltic motion of nanofluids. Carrera et al. [17] checked the extension of a fractional
Let $\rho, \mathbf{U}, \mathbf{F}, \mathbf{W}$ be the density, velocity, body force, and pressure, respectively. The flow parameters for the Jeffrey peristaltic fluid are also supposed to serve as equally good theoretical estimates. xThe different potential fluid mechanical flow parameters for the Jeffrey peristaltic fluid are also supposed to serve as equally good theoretical estimates.

Indeed, the current investigation is firmly believed to receive considerable attention from the researchers towards further peristaltic development with a variety of applications in physiological, modern technology, and engineering.

\[ \rho \left[ \frac{\partial}{\partial t} + \mathbf{U} \cdot \nabla \right] \mathbf{U} + \frac{\partial \mathbf{F}}{\partial t} = \frac{1}{R} \frac{\partial}{\partial R} \left( R \mathbf{S} \mathbf{F}_{\mathbf{rr}} \right) + \frac{\partial}{\partial Z} \left( \mathbf{S} \mathbf{F}_{\mathbf{zz}} \right) - \frac{\mathbf{S}}{R}, \]

\[ \rho \mathbf{S} \mathbf{g} + (\mathbf{C} - C_o) - \sigma \mathbf{D}_{\mathbf{r}} \mathbf{W}, \]

\[ \rho C_P \left[ \frac{\partial}{\partial t} + \mathbf{U} \cdot \nabla \right] \mathbf{T} = K \left[ \frac{\partial^2}{\partial R^2} + \frac{1}{R} \frac{\partial}{\partial R} + \frac{\partial^2}{\partial Z^2} \right] \mathbf{T} + Q_o, \]

\[ \left[ \frac{\partial}{\partial t} + \mathbf{U} \cdot \nabla \right] \mathbf{C} = D_m \left[ \frac{\partial^2}{\partial R^2} + \frac{1}{R} \frac{\partial}{\partial R} + \frac{\partial^2}{\partial Z^2} \right] \mathbf{C} + \frac{D_m K_T}{T_m} \left[ \frac{\partial^2}{\partial R^2} + \frac{1}{R} \frac{\partial}{\partial R} + \frac{\partial^2}{\partial Z^2} \right] \mathbf{T}, \]

\[ \frac{\partial \mathbf{U}}{\partial R} + \frac{\mathbf{U}}{R} + \frac{\partial \mathbf{W}}{\partial Z} = 0. \]
The transformation between these two frames can be written as follows:

\[ r - \bar{r} = 0, \]
\[ z - \bar{z} = -ct, \]
\[ u - \bar{u} = 0, \]
\[ w - \bar{w} = -c. \]  

The relevant governed boundary conditions for the considered flow analysis can be listed as

\[ w + c = 0, \bar{r} = 0 \text{ at } \bar{r} = \bar{r}_1, \]
\[ w + c = 0 \text{ at } \bar{r} = \bar{r}_2 + b \sin \left( \frac{2\pi z}{\lambda} \right), \]
\[ T - \bar{T}_1 = 0, \bar{C} - \bar{C}_1 = 0 \text{ at } \bar{r} = \bar{r}_1, \]
\[ T - \bar{T}_0 = 0, \bar{C} - \bar{C}_0 = 0 \text{ at } \bar{r} = \bar{r}_2. \]  

The leading motion equations of the flow for fluid in the wave frame are given by

\[
\rho \left[ \frac{\partial}{\partial r} + (w + c) \frac{\partial}{\partial z} \right] u + \frac{\partial p}{\partial r} = \frac{1}{r} \frac{\partial}{\partial r} \left( r \bar{S}_{\bar{r}\bar{r}} \right) + \frac{\partial}{\partial z} \left( \bar{S}_{\bar{z}\bar{z}} \right) - \frac{S_{\bar{r}w}}{\bar{r}},
\]
\[
\rho \left[ \frac{\partial}{\partial r} + (w + c) \frac{\partial}{\partial z} \right] w + \frac{\partial p}{\partial r} = \frac{1}{r} \frac{\partial}{\partial r} \left( r \bar{S}_{\bar{r}\bar{r}} \right) + \frac{\partial}{\partial z} \left( \bar{S}_{\bar{z}\bar{z}} \right) + \rho g \alpha_1 (T - T_e) + \rho g \alpha_2 (T - T_e) - \sigma B_0^2 (w + c),
\]
\[
\rho C_p \left[ \frac{\partial}{\partial r} + (w + c) \frac{\partial}{\partial z} \right] T = K \left[ \frac{\partial^2}{\partial r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\partial^2}{\partial z^2} \right] T + Q_o,
\]
\[
\left[ \frac{\partial}{\partial r} + (w + c) \frac{\partial}{\partial z} \right] \bar{C} = D_m \left[ \frac{\partial^2}{\partial r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\partial^2}{\partial z^2} \right] \bar{C} + D_m K_T \bar{T}_m \left[ \frac{\partial^2}{\partial r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\partial^2}{\partial z^2} \right] T,
\]
\[
\frac{\partial p}{\partial r} + \frac{\partial w}{\partial r} = 0,
\]

where \( \bar{S} \) depends only on \( r \) and \( t \). After using the initial condition \( \bar{S}(t = 0) \), we find \( \bar{S}_{\bar{r}\bar{r}} = \bar{S}_{\bar{z}\bar{z}} = \bar{S}_{\bar{r}\bar{z}} = 0 \), and

\[
\left( 1 + \lambda^0, \frac{\partial}{\partial r} \right) \bar{S}_{\bar{r}\bar{r}} = \mu \frac{\partial p}{\partial r}.
\]
We present the following dimensionless parameters for further analysis:

\[\frac{r}{a_2}, \frac{z}{\lambda}, \frac{t}{\lambda}, \frac{u}{c}, \frac{w}{c}, \frac{\lambda_1}{\lambda}, \frac{p}{c\mu}, \frac{\delta}{\lambda}, \frac{\theta}{T - T_0}, \frac{\Theta}{T_1 - T_0} \]

\[\delta = \frac{a_2}{\lambda}, \frac{\Theta}{T_1 - T_0}, \frac{\theta}{T - T_0} \]

\[\Pr = \frac{\mu C_p}{K}, \frac{Re}{\mu}, \frac{Gr}{\mu c}, \frac{Sc}{c\mu}, \frac{Sr}{c\mu}, \frac{Br}{c\mu}, \frac{M}{\mu^2}, \frac{S}{c\mu}, \frac{r_1}{a_2}, \frac{r_2}{a_2} \]

wherever \((\varphi = (b/a_2) < 1)\) is the wave amplitude.

3. Solution of the Problem

For the abovementioned modifications and nondimensional variables listed earlier, the preceding equations are reduced to

\[\text{Re}^3 \left[ u \frac{\partial}{\partial r} + (w + 1) \frac{\partial}{\partial z} \right] u + \frac{\partial p}{\partial z} = \frac{\delta}{r} \frac{\partial}{\partial r} \left( r S_{rr} \right) + \frac{\partial^2}{\partial z^2} \left( S_{rz} \right) - \frac{S_m}{r}, \quad (12) \]

\[\text{Re} \left[ u \frac{\partial}{\partial r} + (w + 1) \frac{\partial}{\partial z} \right] w + \frac{\partial p}{\partial z} = \frac{1}{r^2} \frac{\partial}{\partial r} \left( r S_{rz} \right) + \frac{\partial^2}{\partial z^2} \left( S_{zz} \right) + Gr \theta + Br \Theta - M^2 (w + 1), \quad (13) \]

\[\text{RePr} \left[ u \frac{\partial}{\partial r} + (w + 1) \frac{\partial}{\partial z} \right] \theta = \frac{\theta^2}{Sc} \left[ \frac{\partial^2}{\partial r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\partial^2}{\partial z^2} \right] \theta + \beta, \quad (14) \]

\[\text{Re} \left[ \frac{\partial}{\partial r} + (w + 1) \frac{\partial}{\partial z} \right] \Theta = \frac{1}{Sc} \left[ \frac{\theta^2}{r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\theta^2}{\partial z^2} \right] \Theta + \text{Sr} \left[ \frac{\theta^2}{r^2} + \frac{1}{r} \frac{\partial}{\partial r} + \frac{\theta^2}{\partial z^2} \right] \theta, \quad (15) \]

\[\frac{\partial u}{\partial r} + u \frac{\partial u}{\partial z} + \frac{\partial w}{\partial z} = 0. \quad (16) \]

With boundary conditions

\[w + 1 = 0, u = 0 \text{ at } r = r_1 = \epsilon, \]

\[w + 1 = 0 \text{ at } r = r_2 = 1 + \varphi \sin(2\pi z), \]

\[\theta = 1, \Theta = 1 \text{ at } r = r_1, \]

\[\theta = 0, \Theta = 0 \text{ at } r = r_2. \quad (17) \]

4. The Analytical Solution

Furthermore, the hypothesis of the long wavelength approach is also supposed. Now, \(\delta\) is very small so that it can be tended to zero. Thus, the \(\delta \ll 1\) dimensionless governing equations (12)–(15) by using this hypothesis may be written as
\[
\frac{\partial p}{\partial r} = 0, \quad (18)
\]
equation (18) specifies that \( p \) is only a function of \( z \).

Temperature, concentration, and axial velocity solutions can be described as follows:

\begin{align*}
\theta &= \log \left( \frac{r_y}{r_z} \right) - \beta \left( \frac{r_y^2}{4} \log \left( \frac{r_y}{r_z} \right) - \log \left( \frac{r_y}{r_z} \right) \right), \\
\Theta &= \frac{\text{SrSc} \beta}{4} r^2 + c_3 \log(r) + c_2, \\
\omega &= 4c_2 + 4c_3 \log(r) + f \times \left[ (\frac{dp}{dz})^2 - \frac{\text{Gr} (r_y^2 - 1) \log(r_y) - (r_y^2 - 1)(\log(r_y) - 1) \log(r_y) - (\beta/16)r_y^4)}{4 - f M^2 r^2} \right],
\end{align*}

(19)

(20)

where

\begin{align*}
f &= (1 + \lambda_{in}^2 D_{in}^{n_1}), \\
A &= -4 - f \left[ \frac{d(\log(r_y))}{dz} + \text{Gr} \left( \frac{r_y^2 (\log(r_y) - 1)}{4 \log(r_y) - (r_y^2 - 1)} \right) - \beta \left( \frac{r_y^2}{16} \right)^2 \right], \\
B &= -4 - f \left[ \frac{d(\log(r_y))}{dz} + \text{Gr} \left( -\frac{r_y^2}{4} \log(r_y) - \beta \left( \frac{r_y^2}{16} \right)^2 \right) \right], \\
C_1 &= \frac{4 + \text{SrSc} \beta (r_y^2 - r_z^2)}{4 \log(r_y) - (r_y^2 - 1)}, \\
C_2 &= \frac{\text{SrSc} \beta (r_y^2 - r_z^2)}{4 \log(r_y) - (r_y^2 - 1)}, \\
C_3 &= \frac{(A - B)}{4 \log(r_y)}, \\
C_4 &= \frac{(B \log(r_y) - A \log(r_y))}{4 \log(r_y)}.
\end{align*}

(21)

The heat transfer coefficient is indicated as follows:

\begin{align*}
Zr &= \frac{\partial \theta}{r \partial r} \times \frac{\partial r_y}{\partial z} \\
Zr &= \left[ -\frac{r \beta}{2} + \frac{1}{r \log(r_y)} + \frac{(r_y^2 - r_z^2) \beta}{4 \log(r_y)} \right] \times [2 \varphi \pi \cos(2\pi z)].
\end{align*}

(22)

(23)
Using the definition of the fractional differential operator (5) we find the expression of \( f \) as follows:

\[
f = f(t) = 1 + \lambda_1^{\alpha_1} \frac{t^{\alpha_1}}{\Gamma(1 - \alpha_1)}.
\]  

(24)

5. Results and Discussion

In this section, the effect of different parameters is shown graphically in Figures 2–7 such as fractional parameter \( \alpha_1 \), heat source/sink parameter \( \beta \), wave amplitude \( \varphi \), radius ratio \( \varepsilon \), Hatman number \( M \), Grashof number \( Gr \), relaxation time \( \lambda_1 \), the Soret number \( S_r \), and the Schmidt number \( S_c \) on the temperature \( \theta \), the concentration \( \Theta \), axial velocity \( w \), tangential stress \( s_{rz} \), and heat transfer coefficient \( Z_r \). MATLAB software is used to identify the quantitative influences of various physical parameters implicated in our study. Approximate analytical results are numerically evaluated for temperature, concentration, axial velocity, tangential stress, and the heat transfer coefficient for various values of parameters. For this object, Figures 2–7 are displayed.

Figure 2 has been plotted to clarify the variations of \( \beta \) and \( \varphi \) on the temperature distribution \( \theta \). Figure 2 shows that \( \theta \) decreases when \( \beta \) increases in the range \( 0 \leq r \leq 0.32 \), while \( \theta \) increases when \( \beta \) increases in the range \( 0.32 \leq r \leq 1.2 \). Moreover, \( \theta \) decreases when \( \varphi \) increases in the range \( 0 \leq r \leq 0.32 \), while \( \theta \) increases when \( \varphi \) increases in the range \( 0.32 \leq r \leq 1.4 \). In addition, the temperature decreases with the radial increase and the boundary conditions are fulfilled.

Figure 3 displays the discrepancy of the concentration with the radial for various values of \( \varepsilon, \varphi, S_c \), and \( S_r \). It is indicated that the concentration increases with increasing \( \varepsilon \) and \( \varphi \). However, \( \Theta \) decreases with increasing \( S_r \) and \( S_c \). In addition, the concentration decreases with the radial increase and the boundary conditions are fulfilled.

The impacts of \( Gr, \lambda_1, \varphi, \alpha_1, M, \) and \( S_c \) on the axial velocity \( w \) are illustrated in Figure 4. It is indicated that the axial velocity profiles decrease with increasing \( Gr, \lambda_1, \) and \( \varphi \) in the range \( 0 \leq r \leq 0.32 \), while it increases in the range \( 0.32 \leq r \leq 0.45 \). In addition to this, the axial velocity profile decreases with increasing \( \alpha_1 \) in the whole range \( 0 \leq z \leq 1 \), while it increases with increasing \( M \) in the whole range \( 0 \leq z \leq 1 \). The tangential stress decreases with increasing \( S_c \) in the range \( 0 \leq z \leq 0.53 \) as well, and it increases in the range \( 0.53 \leq r \leq 0.88 \) and then decreases again in the range \( 0.88 \leq z \leq 1 \). It is observed that the velocity has oscillatory behavior due to peristaltic motion concerned.

The effect of \( \alpha_1, M, \beta \) and \( S_c \) can be observed from Figure 5, in which the tangential stress is illustrated for the various values of \( \alpha_1, M, \beta \), and \( S_c \). With the increase of \( \alpha_1 \) and \( S_c \), the tangential stress decreases. Moreover, tangential stress increases with increasing \( M \) and \( \beta \). It is noticed that one can observe the tangential stress is in oscillatory behavior, which may be due to peristalsis.

Figure 6 explains the influence of \( \varepsilon \) and \( \varphi \) on the heat transfer coefficient \( Z_h \). Obviously, the increase in \( \varepsilon \) and \( \varphi \) increases the amplitude of the heat transfer coefficient in the whole range \( z \). From Figure 6, one can observe that heat transfer coefficient is an oscillatory behavior in the whole range, which may be due to peristalsis.

Figure 7 is plotted in 3D schematics concern the axial velocity \( w \), the concentration \( \Theta \), the temperature \( \theta \), and the heat transfer coefficient \( Z_h \) concerning \( r \) and \( z \) axes in the presence \( \alpha_1, S_r, \varepsilon, \) and \( \varphi \). It is indicated that the axial velocity decreases by increasing \( \alpha_1 \). Also, the concentration decreases by increasing \( S_r \), the temperature increases with increasing of \( \varepsilon \) as well, otherwise the heat transfer coefficient increases by increasing \( \varphi \). For all physical quantities, we obtain the peristaltic flow in 3D overlapping and damping when the state of particle equilibrium is reached and increased. The vertical distance of the curves is greater, with most physical fields moving in peristaltic flow.
Figure 3: Discrepancies of the concentration $\Theta$ against the $r$–axis for various values of $\epsilon$, $\phi$, Sc, and Sr.

Figure 4: Continued.
Figure 4: Discrepancies of the axial velocity $w$ against the $r$- and the $z$-axes for various values of $\lambda_1$, $\phi$, $\alpha_1$, $M$, and $Sc$. 

Figure 5: Continued.
Figure 5: Discrepancies of the axial tangential stress $s_{rz}$ against the $z$–axis for various values of $\alpha_1$, $M$, $\beta$, and $Sc$.

Figure 6: Discrepancies of the heat transfer coefficient $Zt$ against the $z$–axis for various values of $\varepsilon$ and $\varphi$.

Figure 7: Continued.
6. Conclusions

The concluding remarks are listed as follows:

1. The axial velocity decreases and increases with the increase of $\alpha_1$, $\phi$, $Gr$, $\lambda_1$, and $Sc$ due to the increase in the Lorentz force.
2. The temperature increases with the increase of the wave amplitude and radius ratio.
3. The concentration decreases with the increase of both $Sr$, $Sc$ and it increases with the increase of both $\varepsilon$ and $\phi$.
4. The tangential stress decreases and increases with the increase of both $\alpha_1$, $Sc$, and it increases with the increase both $M$ and $\beta$.
5. The study of the phenomenon under effect of $\alpha_1$, $\beta$, $\phi$, $\varepsilon$, $M$, $Gr$, $\lambda_1$, $Sr$, and $Sc$ was performed.
6. This study has indeed been widely applied in many fields of science, such as medicine and the medical industry. Thus, in the field of fluid mechanics, it is considered as extremely essential. When inserting an endoscope through the small intestine, this study describes the movement of the gastric juice.

Nomenclature

$R_1, R_2$: Shapes of the wave walls
$t$: Time in a wave frame
$\lambda_1$: Relaxation time
$\alpha_1$: Fractional time derivative parameter
$\gamma$: Rate of the shear strain
$\mathbf{U}, \mathbf{W}$: The components of the velocity in a laboratory frame
$\mathbf{u}, \mathbf{w}$: The components of the velocity in a wave frame
$\mathbf{P}$: The pressure in a laboratory frame
$\mathbf{p}$: The pressure in a wave frame
$\sigma$: Fluid’s electric conductance
$B_0$: The intensity of the external magnetic field
$\rho$: Density
$g$: Gravity constant
$\alpha_c$: Linear coefficient of the thermal expansion
$\alpha$: Coefficient of the viscosity at constant concentration
$c_p$: Specific heat
$K$: Thermal conductivity
$Q_0$: Heat generation coefficient
$\phi$: Wave amplitude in the dimensionless form
$\varepsilon$: Radius ratio
$\Theta$: The distribution of temperature
$\Theta_0$: The distribution of concentration
$T_i, T_f$: Inner and outer tube temperature
$C_i, C_f$: Inner and outer tube concentration
$\delta$: Wavenumber
$\mu$: Fluid viscosity
$M$: Hartmann number
$Re$: Reynolds number
$Pr$: Prandtl number
$Gr$: Grashof number
$\beta$: The heat source/sink parameter
$Br$: Brinkman number
$Sr$: Soret number
$Sc$: Schmidt number.

Data Availability

No data were used to support this study.

Conflicts of Interest

The authors declare that they have no conflicts of interest.

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References

[1] A. M. Abd-Alla, S. M. Abo-Dahab, and H. D. El-Shahrany, "Effects of rotation and initial stress on peristaltic transport of fourth grade fluid with heat transfer and induced magnetic..."
field,” *Journal of Magnetism and Magnetic Materials*, vol. 349, pp. 268–280, 2014.

[2] A. M. Abd-Alla, G. A. Yahya, S. R. Mahmoud, and H. S. Alosaimi, “Effect of the rotation, magnetic field and initial stress on peristaltic motion of micropolar fluid,” *Mechanica*, vol. 47, pp. 1455–1465, 2012.

[3] M. Saqib, H. Hanif, T. Abdeljawad, I. Khan, S. Shafie, and K. S. Nisar, “Heat transfer in MHD flow of Maxwell fluid via fractional Cattaneo-Friedrich model,” *Materials & Continua*, vol. 65, no. 3, pp. 1959–1973, 2020.

[4] Z. Z. Rashed and S. E. Ahmed, “Peristaltic flow of dusty nanofluids in curved channels,” *Materials & Continua*, vol. 66, no. 1, pp. 1012–1026, 2021.

[5] V. P. Rathod and A. Tuljappa, “Slip effect on the peristaltic flow of a fractional second grade fluid through a cylindrical tube,” *Advances in Applied Science Research*, vol. 6, no. 3, pp. 101–111, 2015.

[6] K. Vajravelu, S. Sreenadh, and I. Khan, “Combined influence of velocity slip, temperature and concentration jump conditions on MHD peristaltic transport of a Carreau fluid in a non-uniform channel,” *Applied Mathematics and Computation*, vol. 225, pp. 656–676, 2013.

[7] F. Ali, N. A. Sheikh, I. Khan, and M. Saqib, “Magnetic field effect on blood flow of Casson fluid in axisymmetric cylindrical tube: a fractional model,” *Journal of Magnetism and Magnetic Materials*, vol. 423, no. 4, pp. 327–336, 2017.

[8] J. Zhao, L. Zheng, X. Zhang, and F. Liu, “Convection heat and mass transfer of fractional MHD Maxwell fluid in a porous medium with Soret and Dufour effects,” *International Journal of Heat and Mass Transfer*, vol. 103, pp. 203–210, 2016.

[9] A. M. Abd-Alla, S. M. Abo-Dahab, and A. Kilicman, “Peristaltic flow of a Jeffrey fluid under the effect of radially varying magnetic field in a tube with an endoscope,” *Journal of Magnetism and Magnetic Materials*, vol. 384, no. 15, pp. 79–86, 2015.

[10] Q. Afzal, S. Akram, R. Ellahi, S. M. Sait, and F. Chaudhry, “Thermal and concentration convection in nanofluids for peristaltic flow of magneto couple stress fluid in a non uniform channel,” *Journal of Thermal Analysis and Calorimetry*, vol. 143, no. 2, pp. 56–87, 2021.

[11] T. Hayat and S. Hina, “The influence of wall properties on the MHD peristaltic flow of a Maxwell fluid with heat and mass transfer,” *Nonlinear Analysis: Real World Applications*, vol. 11, no. 4, pp. 3155–3169, 2010.

[12] S. Srivinas and M. Kotheandapani, “The influence of heat and mass transfer on MHD peristaltic flow through a porous space with compliant walls,” *Applied Mathematics and Computation*, vol. 213, no. 1, pp. 197–208, 2009.

[13] M. Ramzan, M. Bilal, and J. D. Chung, “Influence of homogeneous-heterogeneous reactions on MHD 3D Maxwell fluid flow with Cattaneo-Christov heat flux and convective boundary condition,” *Journal of Molecular Liquids*, vol. 230, pp. 415–422, 2017.

[14] H. Rachid, “Effects of heat transfer and an endoscope on peristaltic flow of a fractional maxwell fluid in a vertical tube,” *Abstract and Applied Analysis*, vol. 2015, Article ID 360918, 9 pages, 2015.

[15] M. G. Ibrahim, W. M. Hasona, and A. A. ElShekkhipy, “Concentration-dependent viscosity and thermal radiation effects on MHD peristaltic motion of Synovial nanofluid: applications to rheumatoid arthritis treatment,” *Computer Methods and Programs in Biomedicine*, vol. 170, pp. 39–52, 2019.

[16] E. H. Aly and A. Ebaid, “Exact analytical solution for the peristaltic flow of nanofluids in an asymmetric channel with slip effect of the velocity, temperature and concentration,” *Journal of Mechanics*, vol. 30, no. 4, pp. 411–422, 2014.

[17] Y. Carrera, G. A. Rosa, E. J. Vernon-Carter, and J. Alvarez-Ramirez, “A fractional-order Maxwell model for non-Newtonian fluids,” *Physica A: Statistical Mechanics and Its Applications*, vol. 482, pp. 276–285, 2017.

[18] J. Zhao, “Axisymmetric convection flow of fractional Maxwell fluid past a vertical cylinder with velocity slip and temperature jump,” *Chinese Journal of Physics*, vol. 67, pp. 501–511, 2020.

[19] A. M. Abd-Alla, S. M. Abo-Dahab, and R. D. El-Semiry, “Long wavelength peristaltic flow in a tubes with an endoscope subjected to magnetic field,” *Korea-Australia Rheology Journal*, vol. 25, pp. 107–118, 2013.

[20] D. Tripathi, S. K. Pandey, and S. Das, “Peristaltic flow of viscoelastic fluid with fractional Maxwell model through a channel,” *Applied Mathematics and Computation*, vol. 215, no. 10, pp. 3645–3654, 2010.
[32] S. Hina, T. Hayat, and A. Slsaedi, “Heat and mass transfer effects on the peristaltic flow of Johnson–Segalman fluid in a curved channel with compliant walls,” *International Journal of Heat and Mass Transfer*, vol. 55, no. 13–14, pp. 3511–3521, 2012.

[33] M. Hameed, A. A. Khan, R. Ellahi, and M. Raza, “Study of magnetic and heat transfer on the peristaltic transport of a fractional second grade fluid in a vertical tube,” *Engineering Science and Technology*, *An International Journal*, vol. 18, no. 3, pp. 496–502, 2015.