Computational interfacial rheology

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ABSTRACT

Fluid–fluid interfaces, laden with polymers, particles or other surface-active moieties, often show a rheologically complex response to deformations, in particular when strong lateral interactions are present between these moieties. The response of the interface can then no longer be described by an isotropic surface tension alone. These “structured” soft-matter interfaces are found in many industrial applications, ranging from foods, cosmetics and pharmaceuticals, to oil recovery. Also many biomedical applications involve such interfaces, including those involving lung surfactants and biofilms. In order to understand, design and optimize processes in which structured interfaces are present, flow predictions of how such multiphase systems deform are of the utmost importance, which is the goal of “computational interfacial rheology”, the main topic of this review. We start by rigorously establishing the stress boundary condition used in the computation of multi-phase flows, and show how this changes when the interface is rheologically complex. Then, constitutive models for the extra stress in interfaces, ranging from 2D generalized Newtonian to hyperelastic and viscoelastic, are reviewed extensively, including common pitfalls when applying these models. This is followed by an overview of different approaches to measure interfacial rheological properties, and a discussion of advanced numerical implementations for deforming interfaces. We conclude with an outlook for this relatively young and exciting field.

1. Introduction

Describing multiphase materials or multiphase material flows invariably involves making constitutive assumptions about the propensity of the interface to transmit stress [1–3]. Interfaces can be “simple” and be described by a constant interfacial tension. A first complexity arises when the concentration of surface-active species, which directly control interfacial tension, is changed as a function of time, necessitating a description of the transport phenomena, coupled to the deformation of the interface and the bulk and/or disturbance flows [4]. Further and intrinsic complexity arises when the interface becomes structured, due to an increased dense packing of those objects at the interface or due to lateral interactions between the surface-active moieties which can lead to (transient) network structures [5–10]. Such structured, or complex, soft-matter interfaces respond with extra stresses to a deformation, and linear and nonlinear viscoelastic or viscoplastic rheological properties then emerge which lead to the field of interfacial rheology [3,11,12].

Application areas are broad and diverse, ranging from aerated or multiphase food products [13–17], consumer care products [18], materials in biomedical applications as for example in lung surfactants [19–21], bacterial biofilms [22–24] or in drug delivery applications with monoclonal antibodies [25], and materials in the energy sector such as asphaltenes [26,27] and CO2 storage [28] and finally polymeric materials (foams and blends) [29–31]. Goals of interfacial design are to stabilize products against coalescence [32] or Ostwald ripening [33], to control the morphology of disperse systems and polymeric blends [29], to stabilize multiphase materials [34] or thin film flows [35,36] and to design unit operations such as flotation, foaming, blending and emulsification or - rather the opposite - separations.

In order to understand, design and optimize processes in which structured interfaces are present, flow predictions of how such multiphase systems deform are of the utmost importance, which is the goal of “computational interfacial rheology”. Computational interfacial rheology can contribute to the application areas mentioned above with substantial impact, either societal or economically. For example, a better understanding of the hydrodynamics in the presence of structured interfaces can help further optimizing unit operations. Combined computational and experimental studies can contribute to a better understanding of the role of the stress boundary conditions on thin film behavior and breakup, to improve the understanding of coalescence, breakup and rupture processes in population balance modeling [37,38]. Most drop or bubble deformation studies could be extended to concentrated systems to better understand effects such as avalanches [39] or visco-elastic emulsification [40]. An interplay between processing flows and interfacial rheology can be used to process materials such that non-equilibrium shapes can be locked into designer architectures, and use this in encapsulation or bicontinuous structures [32,41]. Computational rheometry will also be a field that can largely contribute, in particular when analyzing area changing flows, to better underpin the properties measured in, for example, an oscillatory pendant drop experiment [42].

The stability of thin films plays a role in many biological processes as well, which is of unfortunate timely relevance due to the current...
COVID-19 pandemic. A prime example is the stability of the lungs and the lung collapse where a Laplace instability is suggested to occur, which is associated with acute respiratory distress syndrome [21]. Better understanding of these phenomena under dynamic conditions, crucial for improved treatments, would benefit from a computational modeling approach. The same holds true for better understanding of aerosol formation in breathing or sneezing, where the surfactant film in the lungs plays an important role in the production of submicron droplets [43]. Computational interfacial rheology could aid in predicting the size distribution of these droplets and help in designing mitigation strategies. There are many more problems where computational interfacial rheology could have significant impact; to whet the reader’s appetite, some examples are given in Fig. 1.

The measurement of the equations of state and rheological material functions has a long history, going back to iconic scientists such as Ben Franklin, Lord Rayleigh, Agnes Pockels, Joseph Plateau and Irving Langmuir (see the book by Tanford for a historical overview [44]). Methods to measure the linear and non-linear rheological functions at constant surface area have been developed for shear and extensional deformations, as will be reviewed below [45,46], and experiments with clean kinematics and a rigorous separation of bulk and interfacial contributions have been developed, benchmarked and there is clarity on the operating windows where reliable and accurate data can be obtained [47]. The study of the rheological properties in compression or dilution is more challenging as the interplay between the changes in thermodynamic properties, due to changes in surface concentration, and intrinsic compressional viscoelasticity is difficult to deconvolute [48]. Many commercial instruments, such as the popular pendant drop instrument, analyze the response to deformations as if only a surface or interfacial tension is present. As a consequence, the intrinsic material functions are not readily obtained. This calls for computational interfacial rheometrical methods, combining such experiments with computational efforts to deconvolute the effects.

In our opinion, a “perfect storm” is brewing for generating even more broad advances using computational interfacial rheology and fluid mechanics. This review aims to provide firm footing for such progress, starting by laying out the basic assumptions commonly used in interfacial rheology in Section 2, followed by the theoretical description concerning how to set up the boundary conditions for rheologically complex interfaces in Section 3. Whereas the development of constitutive interfaces still allows for further progress, frame invariant descriptions of Newtonian, non-Newtonian, elastic and viscoelastic as well as basic viscoplastic equations are now available; the state of the art for these interfacial constitutive models is reviewed in Section 4. This is followed by a brief introduction to differential geometry in Section 5, which is crucial for the proper mathematical description of interfaces. Then, methods for interfacial rheometry, where numerical methods play an important role in extraction the rheological parameters of the interface, are reviewed in Section 6. Initial results on the simulation of deforming droplets and bubbles as well as drainage and thinning flows are discussed in Section 7, and we end this review with some open problems and an outlook in Section 8.

2. Basic assumptions

In interfacial rheology, the treatment of interfaces is typically done using a continuum approach, where the flow in the bulk of each liquid is described by conservation equations for mass, momentum and energy, and appropriate coupling conditions are employed at the liquid–liquid or liquid–fluid interface. In this “sharp-interface” framework, pioneered by Gibbs, the interface is considered a 2D dividing
To describe the surface extra stress, interfacial constitutive models are needed. Paraphrasing Pozrikidis [56], there are generally three approaches for deriving models that link surface stresses to deformations: (1) the interface is described as a 3D continuum, often assumed incompressible [57], and constitutive equations are derived in the limit of zero thickness, (2) the interface is described as a 2D continuum, and assumptions are made concerning the deformation and stresses in normal direction, possibly yielding non-tangential surface stresses, and (3) the thickness direction is disregarded from the outset, and the interface is described as a 2D surface embedded in 3D space. For many of the interfaces considered in interfacial rheology, it does not seem appropriate to describe interfaces as 2D continua since they are only a few molecules or particles in thickness. We therefore prefer the third approach, which also fits nicely within the framework of Gibbs. Moreover, we mainly treat models that split the constitutive response in an area-preserving part and a distortional part, since these offer much freedom for, e.g. fitting experimental data [58], and using experimentally observable material functions to predict the behavior during flow or deformation.

Using non-equilibrium thermodynamics, tangential slip has been identified as an entropy-producing mechanism for multi-phase systems [52], and may occur for large molecules [59,60]. However, the authors are not aware of reports of interfacial slip for small-molecular systems, suggesting that its magnitude is small enough to be neglected for practical purposes. Hence in most cases it can be assumed that the tangential components of the velocity are continuous across the interface. In addition, it assumed that there is no phase change across the interface, thus only “material interfaces” are considered. The latter assumption implies that the normal velocities are continuous as well, i.e. the velocity vector \( \mathbf{v} \) is continuous across the interface, and we therefore do not introduce a separate interfacial velocity. The 3D position vectors with respect to a chosen origin are denoted by \( \mathbf{x} \), and the subset \( \mathbf{x}_s \) contains those position vectors that point to the interface. A more formal definition of \( \mathbf{x}_s \) will be given in Section 7.1.

3. Momentum balance for complex interfaces

We start by investigating the momentum balance for interfaces, by considering the conservation of the “excess momentum density”. To describe the transport of the surface excess quantities in the sharp-interface framework, an expression for the interfacial conservation law is needed. However, a straightforward generalization from the bulk is complicated due to the possible motion of the interface through 3D space, and the idea of “fixed point on the interface” relying on the non-uniform manner of how we choose to describe the location of the interface [51]. Following Slattery et al. we first introduce the concept of “surface particles” as infinitesimal particles that are bound to the interface, following its motion in 3D space [2]. It can be seen that, by definition, the velocity \( \mathbf{v} \) at the interface is the time derivative of the spatial location, keeping a surface particle constant. With computational interfacial rheology in mind, we follow an approach similar to the arbitrary Lagrangian Eulerian approach [61,62], where the interface is described by a grid that does not necessarily move with the surface particles. An interfacial grid velocity \( \mathbf{v}_g \) is introduced, which is the time derivative of the spatial location, keeping a grid point constant, for which the only requirement is that the grid follows the shape of the interface. This requirement can be expressed as

\[
\mathbf{v}_g \cdot \mathbf{n} = \mathbf{v} \cdot \mathbf{n},
\]

where we note that there are many choices possible for \( \mathbf{v}_g \), and a particular choice is generally motivated by the problem at hand [51]. We are now in the position to define an interfacial material derivative \( \mathbf{D}_i \mathbf{v}_g / \mathbf{D} t \) as the time derivative from the “point of view” of an observer on a fixed surface particle, which yields [2,63]:

\[
\frac{\mathbf{D}_i \mathbf{v}_g}{\mathbf{D} t} = \frac{\partial \mathbf{v}_g}{\partial t} + (\mathbf{v} - \mathbf{v}_g) \cdot \mathbf{\nabla} \mathbf{v}_g,
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\]
where the partial derivative $\partial_i(\cdot)/\partial t$ is for a constant grid point and where $\nabla_s = I_s \cdot \nabla$ is the surface gradient operator (where $\nabla$ is the gradient operator). The velocity $v - v_n$, appearing in Eq. (3), is called the intrinsic viscosity [2] or deformational viscosity [52], and is tangential to the interface, "unaware" of the motion in 3D space.

To derive the momentum balance for interfaces, we proceed along the lines of Leal [1], but we retain the possibility of the interface having dynamical properties of its own and we consider changes in excess momentum. A sketch of an interfacial element $A$ is given in Fig. 3, where we define the normal vector $n$ and the tangential vector $b$.

Note that there are two different tangential vectors, but for brevity will denote them both by $b$ in this section. We assume that there is a bulk fluid present both below and above the interface, with bulk Cauchy stress tensor $\sigma_1$ and $\sigma_2$, respectively. Moreover, as discussed above, we assume that there exists a tangential Cauchy surface stress tensor inside the interface, which we denote by $\sigma_s$, and which is defined by $t_s = \sigma_s \cdot b$, where $t_s$ is the interfacial traction vector.

Collecting all the forces that act on the interfacial element $A$ and identifying them as sources of momentum, we obtain the following excess momentum balance equation [2]:

$$
\frac{d}{dt} \int_A \rho_s \nu dA = \int_A (\sigma_2 - \sigma_1) \cdot n dA + \int_C \sigma_s \cdot b d\ell. \tag{4}
$$

Note that Eq. (4) contains a time derivative over the, possibly time-dependent, surface element $A$. Moreover, the second term on the right hand side is an integral over the contour $C$. To rewrite Eq. (4) in a more useful form, we invoke the surface Reynolds transport theorem and the surface divergence theorem for tangential surface tensors to obtain [2,63]:

$$
\int_A \frac{D\nu}{Dt} dA = \int_A (\sigma_2 - \sigma_1) \cdot n dA + \int_C \nabla_s \cdot \dot{\sigma} d\ell. \tag{5}
$$

where use was made of $D\rho/Dt + \rho(\nabla_s \cdot \nu) = 0$ [53]. The term on the left hand side of Eq. (5) is associated with the inertia of the interface itself, which is typically small, or this term is not even present in the gauge fixed by $\dot{\rho}_s = 0$, and it is generally neglected [47]. Moreover, since Eq. (5) is valid for an arbitrary surface element $A$, we can remove the integrals. Substitution of the general expression for the surface stress tensor, as given in Eq. (1), yields after rewriting:

$$
(\sigma_2 - \sigma_1) \cdot n = \nabla_s \sigma - \nabla(\nabla_s \cdot \nu)n + \nabla_s \cdot \tau. \tag{6}
$$

where the first term on the right hand side represents Marangoni stresses, the second term represents the jump in normal stress due to the curvature of the interface (capillarity), and the last term is due to the extra surface stress (interfacial rheology). To explicitly show the dependence of Marangoni stresses on the equation of state and on spatial variations of the surface excess concentrations, we note that the first term on the right hand side of Eq. (6) can be rewritten for the isothermal case as $V_s \sigma = (\partial \sigma/\partial T) V_s \Gamma$.

Inspired by the nomenclature as introduced by Venerus and Ottinger [52], we will refer to Eq. (6) as the passive momentum balance, whereas Eq. (5) is the integral form of the active momentum balance, with the difference being that the active case involves time-derivatives, which arise due to the left hand side of Eq. (4), whereas the passive case is purely a jump-condition. Similar nomenclatures can be introduced for, e.g., the balance of excess mass or the balance of excess energy.

For deforming curved interfaces, the components of Eq. (6) are most conveniently described in curvilinear coordinates that are not necessarily orthogonal, as will be shown in Section 5. However, it is instructive to investigate Eq. (6) further for a planar interface using the standard Cartesian coordinates $x$, $y$, and $z$. It is assumed that the interface is located in the $xy$ plane, yielding the tangential unit vectors $\mathbf{e}_x$ and $\mathbf{e}_y$ and the normal $\mathbf{n} = \mathbf{e}_z$. The velocity vector is given by $\mathbf{v} = v_x \mathbf{e}_x + v_y \mathbf{e}_y + v_z \mathbf{e}_z$, where we note that $v_z$ is zero at the interface due to the planar assumption. Moreover, we assume that the fluids are Newtonian, thus for the $i$th fluid the stress tensor reads $\sigma_i = -p_i I + 2\eta_i \mathbf{D}$, where $p_i$ is the bulk pressure, $\eta_i$ is the bulk viscosity and $\mathbf{D} = (\nabla \mathbf{v} + (\nabla \mathbf{v})^T)/2$ is the rate-of-deformation tensor. The stress balance in the tangential direction given by $\mathbf{e}_x$ reads:

$$
\eta_i \frac{\partial v_x}{\partial x} |_{1} = \eta_i \frac{\partial v_y}{\partial y} |_{2} = \frac{\partial \sigma_{1x}}{\partial x} + \frac{\partial \sigma_{2x}}{\partial y}, \tag{7}
$$

where the notation $|_i$ means that the term is evaluated at the interface, but on the side of the $i$th fluid. The stress balance in $\mathbf{e}_y$ direction is obtained by exchanging $x$ and $y$ in Eq. (7). The tangential stress balance shows that the discontinuity of the slope of the tangential velocity across the interface is due to a viscosity ratio, Marangoni stresses or interfacial rheological properties, and thus expresses how "stress-carrying" the interface is. In order to describe the interfacial stress tensor $\tau$, constitutive models are needed that link (rate-of-)deformation of the interface to the surface stress, which will be topic of the next section.

4. Interfacial constitutive models

In this section we will review constitutive models for interfaces. The extra surface stresses described by each model are identified with the extra surface stress $\tau$ in Eq. (6).

4.1. Boussinesq-Scriven model

One of the earliest constitutive equations employed for interfaces was obtained by assuming a linear coupling between the interfacial rate-of-deformation and the surface stress [64,65]. The resulting “Boussinesq–Scriven model”, which can be regarded as the surface equivalent of the compressible Newtonian model for bulk fluids, reads in coordinate-free form [2,66]:

$$
\tau = 2\eta_s D_s^2 + \kappa_s (\nabla_s \cdot \nu) I_s, \tag{8}
$$

where $\eta_s$ is the surface (or interfacial) shear viscosity, $\kappa_s$ is the surface (or interfacial) dilatation viscosity, $\nu$ is the velocity vector on the interface and $D_s^2$ is the deviatoric part of the rate-of-deformation tensor $\mathbf{D}_s = (\nabla_s \mathbf{v} + (\nabla_s \mathbf{v})^T)/2$, thus $D_{s}^{2} = \mathbf{D}_{s} - \text{tr}(\mathbf{D}_{s}) I_{s}/2$. The Boussinesq-Scriven model can also be derived by considering the fact that the excess entropy production must be positive, and then seeking for the simplest linear law which ensures this [52]. Note that for some interfaces, shape changes are much easier than area changes, e.g. biological membranes, which makes them effectively incompressible [67]. These systems can also be described by including the surface incompressibility condition $\nabla_s \cdot \nu = 0$ as a constraint, in which case $\kappa_s$ becomes insignificant and $\sigma$ assumes the role of a Lagrange multiplier [68]. Moreover, the presence of a surfactant can also strongly inhibit compression or dilatation of the interface since spatial variations in
surface excess concentration yield interfacial stress gradients, through the equation of state $\alpha F(T)$, that can oppose area changes [4]. Thus the surface incompressibility constraint has been used for surfactant-laden interfaces as well [69]. In this review, we generally allow for changes in area, unless otherwise noted.

In the literature, a number of confusions have arisen concerning the proper form of Eq. (8), which we would like to clarify here. The first is that the velocity vector $\boldsymbol{v}$ as used in Eq. (8) should be the full 3D vector and not only the tangential projection as was done in e.g. [70–74]. It is easy to show that using only the tangential projection cannot be correct: if a sphere or cylinder is blown up by a purely normal velocity at the interface, the interface is clearly deforming and the surface stress should be non-zero. Note, that for planar interfaces, e.g. as studied by Elfring et al., the normal component of the velocity vector at the interface is assumed zero, so using the tangential velocity leads to the correct result [71].

The second point of confusion in literature concerns the projection operation which is applied on $\nabla_{s} \nu$ and $(\nabla_{s} \nu)^T$ in the definition of $\mathbf{D}_s$. This operation is crucial since we define $\nu$ as a tangential tensor, thus the normal components of $\nabla_{s} \nu$ and $(\nabla_{s} \nu)^T$ must be removed before making a direct connection between $\nu$ and $\mathbf{D}_s$ [75]. However, this projection is absent in various works [42, 57, 69–73, 76, 77], for non-planar interfaces this needs to be considered. For certain geometries and situations including the projection might not always lead to significantly different results [42, 78, 79], but it is recommended to remove the normal components of $\nabla_{s} \nu$ and $(\nabla_{s} \nu)^T$.

Again, it is instructive to investigate Eq. (8) further for a planar interface, as was done in Section 3 to emphasize the meaning of the different terms. Substitution of the Boussinesq–Scriven model in the tangential stress balance given by Eq. (7), yields:

$$
\eta_s \frac{\partial \nu_{ys}}{\partial z} = \frac{\partial}{\partial x} \left( \frac{\partial \nu_{ys}}{\partial x} + \frac{\partial \nu_{ys}}{\partial x} \right) + \frac{\partial}{\partial y} \left( \frac{\partial \nu_{ys}}{\partial y} + \frac{\partial \nu_{ys}}{\partial y} \right),
$$

where we assumed $\nu_{yz} = 0$ for brevity. Introducing the velocity scale $V$, length scale $L$, and characteristic surface excess concentration $\Gamma_c$, Eq. (9) can be written in dimensionless form as:

$$
\frac{\partial \nu_{ys}^*}{\partial z^*} = -M a (\partial \nu_{ys}^*/\partial x^*) + B q \left( \frac{\partial^2 \nu_{ys}^*}{\partial x^*} + \frac{\partial^2 \nu_{ys}^*}{\partial y^*} \right) \frac{\partial \theta}{\partial x^*} \left( \frac{\partial \nu_{ys}^*}{\partial x^*} + \frac{\partial \nu_{ys}^*}{\partial y^*} \right),
$$

where $M a = \frac{\partial \nu_{ys}^*/\partial x^*}{\partial \nu_{ys}^*/\partial y^*}$ is the Marangoni number where $(\partial \nu_{ys}^*/\partial y^*)$ will generally depend on $\Gamma_c$, but we treat it here as a constant for simplicity, $B q = \eta_s/(\Gamma_c)$ is the Boussinesq number, $\theta = \kappa_s/\nu_s$ is the interfacial viscosity ratio. Asterisks denote non dimensional variables. Eq. (10) elegantly shows the intricate coupling between interfacial rheology, bulk rheology and transport phenomena. In addition, it shows how the bulk can be regarded as a sink for momentum, with the importance determined by $B q$.

### 4.2. Generalized Newtonian interfaces

In the Boussinesq–Scriven model, as introduced in Eq. (8), it was assumed that the surface viscosities were constant, which has limited applicability for complex interfaces, where the viscosities are generally a function of deformation-rate [80–84] and/or surface excess concentration [4]. A straightforward improvement to the model can be made by assuming that the surface viscosities are a function of the invariants of rate-of-deformation tensor and of $\Gamma$ [66]. To maintain the split into an area-preserving part and a distortional part, we will make use of the first principal invariant of $\mathbf{D}_s$, defined as $I_{D_s} = \text{tr}(\mathbf{D}_s)$, and the second principal invariant of the deviatoric part of $\mathbf{D}_s$, defined as $I_{D_s}^2 = \det(\mathbf{D}_s^2)$, where $\det$ is the surface determinant [2]. It is then assumed that the surface viscosity functions can be written as

$$
\eta_s = \eta_s(I_{D_s}, \Gamma) \quad \text{and} \quad \kappa_s = \kappa_s(I_{D_s}, \Gamma).
$$

The viscosity functions in Eq. (11), are similar to the bulk case [85], such as a power-law or Carreau model, with shear-thinning or shear-thickening behavior determined by the sign of the power-law exponent [84]. Similarly they could be expressed as functions of the invariants of the surface stress tensor.

For a planar interface, a simple shear flow with rate $\gamma$ yields $\mathbf{D}_s = (\gamma/2)(\nu_{s} \nu_{s} + \nu_{s} \nu_{s})$, where $\nu_{s} \nu_{s}$ and $\nu_{s} \nu_{s}$ are the orthonormal tangent and normal tangent unit tensors as introduced in Section 3. An isotropic flow with area rate of change $\theta$ yields $\mathbf{D}_s = (\theta/2)(\nu_{s} \nu_{s} + \nu_{s} \nu_{s})$, where $\theta > 0$ for surface dilatation and $\theta < 0$ for surface compression. It can thus easily be verified that the first invariant of $\mathbf{D}_s$ is the area rate of change, whereas the second invariant of $\mathbf{D}_s^2$ is related to the rate of shear. Using the invariants of $\mathbf{D}_s$ and $\mathbf{D}_s^2$, other non-Newtonian behavior, typically inspired by models for bulk rheology, can be carried over to interfaces in a rather straightforward manner [66, 82]. To illustrate this, we present here, as an ansatz, the compressible Bingham model for viscoplastic interfaces, which is based on the bulk counterpart of this model [86–88], but maintaining the deviatoric-isotropic split. The deviatoric surface stress is given by:

$$
\tau_{vy} = 2 \eta_s \mathbf{D}_s^2 + \frac{2 \eta_s}{| \mathbf{D}_s^2 |} \tau_{vy} \quad \text{if } | \mathbf{D}_s^2 | > 2 \tau_{vy},
$$

$$
\tau_{vy} = 0 \quad \text{if } | \mathbf{D}_s^2 | \leq 2 \tau_{vy},
$$

where $| \mathbf{D}_s^2 | = \sqrt{2 \text{tr}(\mathbf{D}_s^2)^2}$ is the magnitude of the deviatoric rate-of-deformation tensor, $| \tau_{vy} | = \sqrt{2 \text{tr}(\tau_{vy}^2)}$ is the magnitude of the deviatoric surface extra stress tensor and $\tau_{vy}$ is the shear yield stress. Note that $| \mathbf{D}_s^2 |$ and $| \tau_{vy} |$ can also be expressed as functions of the principal invariants introduced above. For the isotropic part of the surface stress we obtain:

$$
\text{tr}(\tau_{vy}) = 2 \nu_s (\nu_s \cdot \nu_s + \nu_s \cdot \nu_s) \tau_{vy} \quad \text{if } | \text{tr}(\tau_{vy}) | > 2 \tau_{vy},
$$

$$
\nu_s \cdot \nu_s = 0 \quad \text{if } | \text{tr}(\tau_{vy}) | \leq 2 \tau_{vy},
$$

where $\tau_{vy}$ is the isotropic yield stress, i.e. the yield stress in compression/dilatation. Using the notation from the previous paragraph, the model predicts in simple shear:

$$
\tau_{vy}(\nu_y) = \nu_s \theta + \frac{\gamma}{| \theta |} \tau_{vy} \quad \text{if } | \tau_{vy}(\nu_y) | > \tau_{vy},
$$

$$
\gamma = 0 \quad \text{if } | \tau_{vy}(\nu_y) | \leq \tau_{vy},
$$

where $\tau_{vy}(\nu_y) = \nu_s \nu_s \cdot \nu_s$, and similarly for the other components of $\tau_{vy}$. In dilatation/compression the model predicts:

$$
\tau_{vy}(\nu_y) = \nu_s \theta + \frac{\gamma}{| \theta |} \tau_{vy} \quad \text{if } | \tau_{vy}(\nu_y) | > \tau_{vy},
$$

$$
\theta = 0 \quad \text{if } | \tau_{vy}(\nu_y) | \leq \tau_{vy}.
$$

Similar to the bulk counterpart of the model, the yield stress can be a function of, e.g., a structural parameter [57] or the surface concentration [88]. Moreover, the yield criterion as used in Eq. (12) is a “von Mises-like” criterion for interfaces, whereas the yield criterion in Eq. (13) depends on isotropic contributions and thus differs from the von Mises criterion [89]. Although the Bingham model for interfaces has been successfully used for area-preserving flows [82, 90, 91], we are not aware of any other experimental/numerical work that employs the Bingham model for interfaces with area-changing flows in the form given here. Although conceptually quite different from, e.g. the power law model, we categorized the interfacial Bingham model as a generalized Newtonian model since the effective viscosity is only a function of the instantaneous rate of deformation, albeit in a discontinuous manner. Thorough investigations into thermodynamic consistency, experimental validation and numerical stability, especially for area-changing flows, will be crucial for it to be as successful as its bulk counterpart [92].
Besides the deformation rate, the surface excess concentration \( \Gamma \) can affect the value of the viscosity [93–95]. This dependency is typically described by an exponential relation between the viscosity and the surface pressure, where the latter is defined by \( \Pi = \sigma - \sigma(T) \), with \( \sigma \) the interfacial tension of the clean interface. Depending on the system under consideration, both \( \Pi \)-thinning and \( \Pi \)-thickening interfaces exist [4]. To describe the distribution of \( \Gamma \) at the interface, an additional interfacial balance equation is needed, which can be readily derived in a similar manner as the momentum balance in Section 3. In the absence of reactions, and assuming Fick’s law for diffusion at the interface, conservation of mass yields the following surface-convection–diffusion equation:

\[
\frac{D_\Gamma}{Dt} + \nabla \cdot (\Gamma \mathbf{v}_s) = \alpha \mathbf{v}_s \nabla^2 \Gamma + j_n,
\]

where \( \alpha \) is the surface diffusion coefficient and \( j_n \) is a source term that describes adsorption/desorption from and to the bulk. Often, the grid velocity is chosen equal to the normal velocity of surface particles, which yields [96]:

\[
\frac{\partial \Gamma}{\partial t} + \mathbf{v}_s \cdot (\Gamma \mathbf{v}_s) = \alpha \mathbf{v}_s \nabla^2 \Gamma + j_n,
\]

where \( \mathbf{v}_s = \mathbf{I} \cdot \mathbf{v} \) is the tangential interface velocity and \( \mathbf{v} \) is the magnitude of the normal velocity \( \mathbf{v}_n = \mathbf{n} \cdot \mathbf{v} \). Adsorption/desorption is mainly important for small-molecular surface active agents, that typically do not exhibit interfacial rheological behavior [95]. However, because changes in \( \Gamma \) lead to changes in surface tension through the equation of state \( \sigma(T, \Pi) \), a time-dependent interfacial tension can exist for these systems. Historically, this effect has often been described using a complex interfacial modulus [97] which is readily obtained using an oscillatory pendant drop instrument. We will not do that here, however, since the resulting parameters are not rheological material functions, but they are related to transport phenomena, as is clear from the fact that they are geometry dependent [98,99]. From a computational perspective, the material parameters that control this time dependence, and thus should be used as inputs in the modeling, are the bulk diffusivities and energy barriers for adsorption (interaction potentials). Rheological material functions should only relate stress to only strain or strain rate, and these are easily identified for structured, yet passive interfaces. Reporting apparent interfacial moduli, which arise due to time dependent properties and the diffusion to/from an active interface, in terms of properties of a passive interface have obfuscated the field of interfacial rheology and how to use any experimental data in a predictive modeling efforts. Further discussion on this topic can be found elsewhere [3,46,100].

### 4.3. Elastic interfaces

Elastic interfacial constitutive models can be constructed that couple the surface stress to the deformation with respect to some reference state. Although interfacial structure could in principle lead to anisotropic interfacial elasticity, for simplicity only isotropic elasticity is considered here, implying that the surface stress and surface strain are coaxial [57]. We introduce the stretch ratio \( \lambda \), which describes the change in length of a line \( dX_s \), tangential to the surface in the deformed state, relative to a line \( dX \), tangential to the surface in the reference state: \( \lambda = (dX_s / dX) / (dX_s / dX) \), where \( X_s \) and \( X \) are the position vectors to the interface in the deformed and reference configuration, respectively. For small deformations, the linear surface strain tensor can be used to construct constitutive equations, which is defined by \( U_s = (\nabla \mathbf{u} - \mathbf{I}) + (\nabla \mathbf{u}) / 2 \), where \( \mathbf{u} \) is the 3D displacement vector on the interface. For small deformations, the principal values of \( U_s \) are \( \epsilon_1 = \lambda - 1 \) and \( \epsilon_2 = \lambda^2 - 1 \), where \( \epsilon_1 \) and \( \epsilon_2 \) are the two in-plane principal linear strains and \( \lambda_1 \) and \( \lambda_2 \) are the two in-plane principal stretch ratios. For linear elastic behavior, we can define a strain-energy area density function of the form [57]

\[
W_S(\epsilon_1, \epsilon_2) = G_s (\epsilon_1^2 + \epsilon_2^2) + \frac{1}{2} (K_s - G_s) (\epsilon_1 + \epsilon_2)^2.
\]

where \( G_s \) is the interfacial shear modulus and \( K_s \) is the interfacial dilatational modulus. By taking the derivative of \( W_s \) with respect to the linear strain, we obtain the stresses acting on an infinitesimal patch of the interface, similar to the approach in bulk [101]. The resulting stresses can be written in tensor form to yield Hooke’s law for linear elastic interfaces [76]:

\[
\tau_{11} = 2G_s U^d_1 + K_s (\mathbf{v}_s \cdot \mathbf{n}) I_s,
\]

where \( U^d_1 \) is the deviatoric part of linear strain tensor: \( U^d_1 = U_1 - \mathrm{tr}(U_1) I_s / 2 \). Alternatively, Eq. (19) can be written in terms of the interfacial Lamé constants, Young’s modulus or Poisson ratio [48,75,102]. Note, that Eq. (19) is sometimes written with additional 1/4 terms, which arise due to the area change between the deformed and reference state [103]. However, since Eq. (19) derives from the theory of linear elasticity, it is only valid for infinitesimal deformations and, to first order, no distinction is made between the deformed and reference state. To go beyond the small deformation limit, finite strain tensors are needed.

In the literature, isochoric “Mooney–Rivlin” or “neo-Hookean” models are often derived by assuming that the membrane has a finite thickness and adding the assumption that the membrane deformation is volume-preserving [104]. The strain-energy volume density function, together with the isochoric condition \( \lambda_1 \lambda_2 \lambda_3 = 1 \), where \( \lambda_i \) is the stretch ratio in the normal direction, yields hyperelastic interfacial models. However, these models generally have limited usefulness, mainly because they lack an independent parameter to describe the constitutive response to dilatational/compression of the interface [57]. Moreover, the assumption of a continuum in the thickness direction is questionable for systems that only consist of one to a few molecules or particles in thickness direction [56].

Alternatively, the thickness direction can be neglected completely, and the membrane elasticity can be formulated in terms of a strain-energy area density function. Here, we give two of such models which are particularly useful since they both employ a split in the isotropic and shear response. Both models can be written in terms of the left Cauchy–Green interfacial strain tensor \( B_s = F_s^\text{T} F_s \), where \( F_s \) is the 2D interfacial deformation gradient tensor given by \( F_s = \mathbf{d} \mathbf{x}_s / \mathbf{d} \mathbf{x} \). Note that \( B_s \) is symmetric and tangential to the surface in the deformed state. Furthermore, \( J \) is the relative area deformation, which can be written as \( J = \det(\mathbf{F}_s) = \lambda_1 \lambda_2 \lambda_3 \). The first is the Evans–Skalak model, which is often used for the modeling of bio-membranes, and for which the strain-energy area density function with respect to the reference state is given in terms of the principal stretch ratios as [105]:

\[
W_{ES} (\lambda_1, \lambda_2) = G_s \left( \frac{\lambda_2^2 + \lambda_1^2}{2} - 2 \right) + \frac{K_s}{2} (J - 1)^2,
\]

where \( J = \lambda_1 \lambda_2 \) is the relative area deformation. More recently, a new constitutive equation was derived by Pecicelli et al. [58], with the notable difference that a Hencky strain measure is used for the isotropic deformation, which is known to be able to describe moderate non-linearities and has the additional advantages that it is symmetric in dilatation/compression and additive [48]:

\[
W_{NH}(\lambda_1, \lambda_2) = G_s \left( \frac{\lambda_2^2 + \lambda_1^2}{2} - 2 \right) + \frac{K_s}{2} \ln J^2.
\]

From the strain area density functions, the surface stresses can readily be calculated [58]. For the strain area density function as given by Eq. (21) this yields the neo-Hookean model for compressible interfaces, which reads in coordinate-free form [58]:

\[
\tau_{NH} = \frac{G_s}{J} B^T + K_s \ln(J) I_s.
\]

where \( B^T = B_s - \mathrm{tr}(B_s) I_s / 2 \) is the deviatoric part of the left-Cauchy–Green interfacial strain tensor at constant area, which is given by \( B_s = \mathbf{B}_s / J \). For the Evans–Skalak model as given by Eq. (20), the deviatoric part of the surface stress is similar to Eq. (22), but the isotropic part is given by \( K_s (J - 1) I_s \). A comparison of different strain measures for describing the isotropic deformation of the interface is shown in Fig. 4.
4.4. Viscoelastic interfaces

Similar to bulk rheology, linear viscoelasticity of interfaces can be introduced by integrating the rate of deformation over all past times multiplied with decaying relaxation moduli [106]. The deviatoric and isotropic parts of the linear viscoelastic surface stress can then be written as [107]:

\[
\tau_{\text{ve}}^d = \int_0^\infty 2G(t - \tau) D_\tau^d(\tau) d\tau, \quad \text{tr} (\tau_{\text{ve}}^d) = \int_0^\infty 2K(t - \tau) \text{tr}(D_\tau^d(\tau)) d\tau,
\]

(23)

where \( \tau_{\text{ve}}^d \) denotes the deviatoric part of the linear viscoelastic surface stress and where \( G(t) \) and \( K(t) \) are the relaxation moduli for shear and dilation/compression, respectively. The constitutive relations given by Eq. (23) are the general linear viscoelastic model for interfaces, which can be used to, e.g., define the complex interfacial viscosity of the interface, in a similar way as their bulk counterparts [108].

The relaxation moduli can be estimated using the Maxwell model as exponentially decaying functions:

\[
G(t) = G_0 e^{-t/\lambda_s}, \quad K(t) = K_0 e^{-t/\lambda_d},
\]

(24)

where \( G_0 \) and \( K_0 \) are the instantaneous shear and bulk moduli, respectively, and \( \lambda_s \) and \( \lambda_d \) are the relaxation times in shear and dilation/compression respectively. Extension of this model to multiple relaxation processes is straightforward, and can be done by including multiple modes [106]. Similar to bulk rheology, this general linear viscoelastic model can be used to describe small-strain experiments such as creep recovery and stress relaxation after step strains. The latter approach was used to verify the Boltzmann superposition principle, one of the pillars of linear viscoelasticity, for a polymer multilayer at the air–water interface under isotropic compression, where the extra stress was more important compared to the thermodynamic one [109] (see Fig. 5).

Other constitutive models, based on linear viscoelasticity, such as the linear Kelvin–Voigt and Jeffreys models, can be readily derived following typical approaches from bulk-rheology, leading, e.g., to the surface upper-convected Maxwell (SUCM) model, which describes the evolution of the deviatoric viscoelastic stress, denoted by \( \tau_{\text{ve}}^d \), by the following evolution equation [53,107,117]:

\[
\dot{\tau}_{\text{ve}}^d + \lambda_d \tau_{\text{ve}}^d + \lambda_s (\nabla_s \cdot \tau_{\text{ve}}^d)\nabla_s + \lambda_s (\nabla_s \cdot \tau_{\text{ve}}^d)\nabla_s = 2\eta_s D_s^d.
\]

(25)

where the surface upper convected derivative is defined as

\[
\dot{\psi}(\cdot) = \frac{D_s(\nabla_s \cdot \cdot \cdot)}{Dt} - (\nabla_s \cdot \cdot \cdot) (\cdot) \cdot \nabla_s \cdot \cdot \cdot.
\]

(26)

Note that the surface upper convected derivative, as we define it here, is different from the one found often in the literature, which includes additional projection operations [53,107,117,118]. In Appendix, we show that the form including the additional projections is not frame invariant, whereas the form given in Eq. (26) is frame invariant, thus we believe the latter to be correct. Moreover, the third term on the left hand side of Eq. (25) is absent in the original presentation of the SUCM model [107,117], but it is added to ensure that \( \tau_{\text{ve}}^d \) remains traceless [53,119–121]. The evolution of the isotropic part of \( \tau_{\text{ve}} \) can be written as [107]:

\[
\lambda_d \frac{D_s(\nabla_s \cdot \tau_{\text{ve}})}{Dt} + \text{tr}(\tau_{\text{ve}}) = 2\kappa_s \text{tr}(D_s),
\]

(27)

where \( \kappa_s \) is the surface (or interfacial) dilatation viscosity. The SUCM model presented here is in a convenient form due to the split between the deviatoric and isotropic parts. However, similar to the case of bulk viscoelasticity [120], other variants of the SUCM could be constructed as well, that treat the isotropic part in different ways. Moreover, extensions can be made to this model to include, e.g., shear-thinning, yielding the interfaceal Giesekus model [53,107]. Despite their success for bulk rheology, there is, as far as the authors know, no experimental literature using these non-linear viscoelastic models, and numerical work is scarce and often uses the incorrect form of the SUCM model [118].

Fig. 4. Comparison of different strain measures for describing the isotropic deformation of the interface. Here \( A \) denotes the current surface area and \( A_0 \) denotes the surface area in the reference state.

Fig. 5. Boltzmann superposition principle in 2D: Normalized surface pressure versus time for isotropic step compression experiments on PVP/PMAA multilayers at the air–water interface with three incremental Hencky strains of \(-2\%\). Experimental and modeling results of a large step of \(-6\%\) is also included. The dashed red lines are the theoretical predictions and the black solid lines the experimental data. The lighter colored lines indicate the response to a single step strain of \(-6\%\).

Source: Reprinted with permission from [109]. © 2019 The Society of Rheology.
4.5. Interfaces with resistance to bending

Bending stresses are important for biological membranes [122], but recently have also been shown to play a role for particle-laden interfaces, since they can have non-zero bending moduli, as observed in e.g. graphene oxide sheets [114], microparticles [123] or nanoparticles [124]. To describe the resistance against bending, the starting point is typically the Helfrich Hamiltonian, which assumes that the bending energy is quadratic in the mean curvature minus the spontaneous energy is quadratic in the mean curvature minus the spontaneous curvature and linear in the Gaussian curvature [125]:

\[
F_B = \iint A B (H_m - H_0)^2 \, dA + \oint A B G H \, dA.
\]  

(28)

where \(B\) and \(B G\) are the bending moduli, \(H_m = V_s \cdot n / 2 = (\kappa_1 + \kappa_2) / 2\) is the mean curvature, where \(\kappa_1\) and \(\kappa_2\) are the principal curvatures, \(H_0\) is the mean spontaneous curvature and \(H_G = \kappa_1 \kappa_2\) is the Gaussian curvature. Variational procedures lead to a force density of the form [126,127]:

\[
f_B = 2B \left[ V_s \cdot (H_m - H_0) + 2(H_m - H_0)(H_G + H_0 H_m) \right] n + 2BV_s [(H_m - H_0)^2].
\]  

(29)

where it was assumed that no topological changes occur, thus, due to the Gauss–Bonnet theorem, the second term in Eq. (28) is a constant which does not lead to a force density. The tangential term in Eq. (29) is often neglected, but, e.g. red blood cells in flow, its magnitude is small compared to the tangential elastic stress, or it can be absorbed in the surface pressure if the interface is incompressible [126].

The force density as given by Eq. (29) can be readily incorporated in numerical simulations, i.e. it is added to Eq. (6) as a jump in traction [126,128,129]. Moreover, \(f_B\) can be written as the surface divergence of a surface stress tensor \(\tau_s\), which can be added to the surface stress \(\tau \) [57,122,130]. The force density then becomes a surface force in the direction of the surface normal which is transverse to the surface [133]:

\[
\mathbf{V}_s = \mathbf{g}_s \cdot \frac{\partial}{\partial \mathbf{x}},
\]  

(30)

where \(\mathbf{g}_s\) and \(\mathbf{g}_s\) form a basis that is not necessarily orthogonal, nor are their lengths necessarily normalized. The dual basis vectors \(\mathbf{g}^i\) are defined by

\[
\mathbf{g}_i \cdot \mathbf{g}^j = \delta_i^j,
\]  

(32)

where \(\delta_i^j\) is the Kronecker delta. Any vector or tensor that is tangential to the surface, denoted by \(a\) and \(A\) respectively, can thus be written as

\[
a = a^i \mathbf{g}_i, \quad A = A^i \mathbf{g}_i \mathbf{g}^j \mathbf{g}^j.
\]  

(33)

where \(a^i\) and \(a^j\) are the contravariant and covariant components of the vector \(a\), respectively, and \(A^i\) and \(A_j\) are the contravariant and covariant components of the tensor \(A\), respectively. Moreover, the surface gradient operator can be written as

\[
\mathbf{V}_s = \mathbf{g}_s^i \frac{\partial}{\partial \mathbf{x}^i}.
\]  

(35)

And finally, we can write for the surface unit tensor

\[
I_s = s_i^j g^j g^j = s_i^j g^j g^k = s_i^j g^j g^k = g^j g^k.
\]  

(36)

where the metric matrix \(s_{ij} = g^i \cdot g^j\) and the dual metric matrix \(s^{ij} = \mathbf{g}_i \cdot \mathbf{g}_j\) were introduced.

To describe the velocity \(v\) and position of the interface \(x_s\), we make use of the standard Cartesian basis, thus \(v = v_i e_i\) and \(x_s = x_i e_i\), where the index is identified with the Cartesian coordinates \(x, y\) and \(z\). For example the surface gradient of the velocity can be written as [133]:

\[
\nabla_s v = \frac{\partial v_i}{\partial x^i} (\mathbf{g}^i \cdot \mathbf{e}_i e_i e_i).
\]  

(37)

and for the surface divergence of the velocity:

\[
\nabla_s v = \text{tr}(\nabla_s v) = \frac{\partial v_i}{\partial x^i} (\mathbf{g}^i \cdot \mathbf{e}_i).
\]  

(38)

The expressions in Eqs. (37) and (38) are particularly useful since they show how the surface operations can be written in terms of the Cartesian components of the velocity, natural/dual basis vectors and position vector, and can thus be incorporated in any standard numerical method for 3D bulk flow.

Orthogonal curvilinear coordinates

We conclude our brief treatment of differential geometry by investigating the special, but very important case of orthogonal curvilinear coordinates, where we have by definition:

\[
g_i \cdot g_j = \delta_i^j, \quad \text{for} \quad i \neq j.
\]  

(39)

It is often more convenient to normalize the natural basis vectors:

\[
e_i = h_i g_i, \quad \text{(no summation)}.
\]  

(40)

where \(h_i = (\mathbf{g}_i \cdot \mathbf{g}_i)^{-1/2} \) (no summation) are the scale factors, also known as the metrical coefficients [66]. Note that the normalized natural basis vectors coincide with the normalized dual basis vectors, and we thus do not distinguish between contravariant and covariant components when using orthonormal basis vectors. The set of unit tangential vectors \(e_1\) and \(e_2\) and unit normal vector \(n\) forms a useful basis for interfacial rheology, and the resulting components of vectors/tensors are referred to as the physical components [2]. Moreover, the surface gradient operator can be written as

\[
\mathbf{V}_s = \sum_{i=1}^2 e_i \frac{\partial}{\partial x^i} h_i \frac{\partial}{\partial t},
\]  

(41)

which allows one to write the surface derivative operations in a more convenient form [66]. The scale factors for standard coordinate systems such as cylindrical- and spherical coordinates are well-documented, see e.g. [108,131,134], and are useful for cases where the interface does not deform and coincides with one of the coordinate surfaces, as we will show in the next section. Clearly, for the Cartesian coordinate system, all the scale factors are one, and the basis vectors are constant in space.
6. Methods for interfacial rheometry

Due to the inherent hydrodynamic coupling of the interface with the bulk, as shown by Eq. (6), it is generally not possible to obtain a direct universal rheometric flow at the interface, i.e. a flow with a known surface (rate-of-)deformation tensor. The bulk fluids act as a sink for the interfacial momentum, with the ratio between the bulk and interfacial transport depending exactly on the a priori unknown interfacial rheological properties. Analytical and numerical methods are therefore crucial for calculating the flow field in a given geometry, and thus the velocity field at the interface. With the deformation rates at the interface known, rheological properties of the interface can be inferred by investigating the response of the probe, e.g. displacement or force/torque [46]. A large range of experimental setups is available for interfacial rheometry, a complete overview of which is beyond the scope of the current review. Extensive reviews are available in the literature [3,46,135]. The methods in this section have in common that they assume that the interface retains a fixed shape, allowing for a description in orthonormal coordinates, as introduced in Section 5. Moreover, by benefitting from symmetries occurring naturally in the problem, the governing equations and numerical methods for solving them are simplified considerably.

6.1. Interfacial shear flows

Several experimental setups are available for the generation of an interfacial shear flow, without the effects of compression/dilatation; here we will discuss a number of them. Among the first proposed geometries, were ones where an interfacial shear flow was generated by lowering a disk or bicone geometry into an interface, and rotating the cup that held the fluids [136]. Torques on the disk could be measured using, e.g., a torsion wire. For these geometries, Oh and Slattery [136] applied the Boussinesq–Scriven model for the surface stress and the Stokes equation for the bulk flow, neglecting effects from inertia. An implicit solution was obtained for the velocity field, and an iterative numerical scheme was applied to calculate the interfacial viscosity based on the measured torque on the probe in steady shear. This approach was later extended for sinusoidal deformations [137], and linear surface viscoelasticity can be investigated in the same geometries by [138] and [139], by assuming that the viscosity in the Boussinesq–Scriven model was complex. Erni et al. extended the analysis of Oh and Slattery, and proposed a bicone fixture that could be used in standard rotational rheometers [140]. Moreover, they introduced an improved numerical scheme that allowed for the calculation of the velocity field for a given torque, which can be used to infer interfacial properties, but fluid inertia was still neglected. A recent analysis of the bicone geometry was provided by Tajuelo et al., who used a finite-difference scheme to numerically calculate the flow in the bulk and at the interface and which does take inertia into account [141]. The same group later made the code, called BiconeDrag, freely available [142].

However, accurate measurements using the disk or bicone geometries are limited to interfaces with high interfacial viscosities as compared to the bulk viscosity [47]. This becomes immediately clear when defining a macroscopic Boussinesq number as [46,143,144]:

$$\text{Bq} = \frac{\eta_s \frac{v}{L_b} P_s}{\eta_b \frac{v}{L_s} A_b} = \frac{\eta_s}{\eta_b} \frac{L_b A_b}{L_s A_s} q_s a.$$  

where \(V\) is a characteristic velocity, \(L_s\) and \(L_b\) are the characteristic length scales at which the velocity decays at the interface and in the bulk phase, respectively, \(P_s\) is the contact perimeter between the rheological probe and the interface, and \(A_s\) is the contact area between the probe and the bulk phase. The parameter \(a = L_s A_b/(L_b P_s)\) has units of length, and shows how the Boussinesq number can be effectively increased by, e.g., increasing the perimeter of the probe or decreasing its surface area in contact with the bulk. A geometry with a smaller value of \(a\), thus an increased sensitivity, is the double wall ring (DWR) setup, which was proposed by Vandebril et al. [145]. In their analysis, the Navier–Stokes equation was solved in the bulk and coupled to the flow at the interface, using finite-differencing schemes on 2D meshes, which was made possible by the radial symmetry of the problem. This approach included effects of inertia, and the response of the interface was described using the Boussinesq–Scriven model with real or complex viscosities. Interfacial viscosities could be inferred by matching boundary conditions between the simulations and the experiments in an iterative manner. The numerical codes were made freely available [145]. Another approach for decreasing \(a\), thus increasing the sensitivity, is using a “knife edge geometry”, and similar numerical approaches to take the bulk flow into account for this geometry, typically using finite differencing methods, are published in the literature [83,146,147].

Another geometry for shear interfacial rheology consists of a (micro)needle at an interface, which is moved by a known magnetic force, as proposed by Brooks et al. [143]. With this setup, which is commonly called the interfacial shear rheometer (ISR), the interfacial viscosity can be calculated from the displacement of the needle, for example for sinusoidal oscillations of the force. Brooks et al. assumed that \(Bq \gg 1\), such that a linear velocity profile is generated at the surface, i.e. all the dissipation occurs in the interface. To allow for measurements at lower values of \(Bq\), Reynaert et al. proposed a numerical calculation of the flow field for linear-elastic interfaces, which takes the full flow in the bulk, including effects of inertia, into account [148]. In this manner, measurements at lower values of \(Bq\) became accessible, also for the ISR. This approach was later verified by Verwijlen et al. using a point force solution at the interface [144]. The accuracy of the ISR can be improved by decreasing the needle size, thus decreasing the value of \(a\) [149]. Finally, we note that more advanced numerical approaches have become available for the ISR, such as a boundary element method [150], who reported results in good agreement with previously mentioned works (see Fig. 7).

The high aspect ratio of the (micro)needle used in the ISR ensures that end effects play a negligible role. Disk-shaped interfacial probes
can be used to generate an interfacial shear flow by rotation inside the interface, for example by magnetically applying a torque to a ferromagnetic “microbutton” [93,151–154]. Translation of probes with an aspect ratio of $O(1)$ at planar interfaces induces a mixed flow field, which makes the analysis significantly more difficult; these will be discussed in Section 6.3.

Rheometers that probe different deformation modes, typically inspired by bulk rheometers, have also been proposed. For example, the Cambridge Interfacial Tensiometer [155,156] is a 2D equivalent of a filament stretching rheometer. Although this device would ideally operate at constant surface area, the numerical/experimental analysis by Verwijlen et al. showed that the interfacial flow field contains dilational, shear and extensional components, depending on the ratio of the material parameters [157]. They conclude that these type of “mixed flows” contain a wealth of rheological information, but are typically difficult to analyze, limiting their accuracy. In a follow-up work, similar conclusions were drawn for the interfacial rheometer consisting of a ring-like fixture for the DWR with undulations that produces a more controlled mixed flow field “by design” [158]. A typical feature of such a mixed flows, is that the flow field is dominated by the “cheapest” deformation mode, i.e. the one for which the viscosity is lowest, which inherently leads to a low sensitivity [158].

6.2. Area-changing flows

Whereas the experimental and numerical methods for flows at constant surface area are well-established, the development of dilational/compressional rheometry is not so far. The main difficulty lies in obtaining a truly isotropic deformation of the interface, without any effects of shear [46]. Historically, the drop-shape analysis of a pendant drop is the technique that is most often used to investigate the response of the interface to dilation/compression. Note that the same analysis also applies to rising bubbles, but for brevity we will only talk about pendant drops in this section. With the pendant drop setup, the surface tension is obtained by fitting the Young–Laplace equation to the shape of the drop, which can be easily obtained from Eq. (6) by assuming only hydrostatic contributions to the bulk stress and in the absence of deviatoric surface stresses. Therefore, the Young–Laplace equation assumes an isotropic and constant surface stress, and small capillary- and inertial relaxation times such that the shape is in equilibrium. Moreover, the deformation of the drop due to gravity must be large enough in order to obtain an accurate value of the surface tension [159]. By oscillating the volume of the drop, the interface deforms in a complex, mixed manner which includes shear and dilation/compression, as shown in the FEM simulations by Balemans et al. [42] and reproduced in Fig. 8. The surface deformation yields a change in the surface excess concentration $\Gamma$, and thus the surface tension through the equation of state $\sigma(\Gamma, T)$. This effect is commonly called Gibbs elasticity, but its origin is generally different then, e.g., the origin of hyper- and viscoelasticity as introduced in Sections Section 4, which arise due to lateral interactions between surface-active moieties [48]. The response of the interfacial tension for systems with small molecular surfactants is often time-dependent, which is due to the relaxation processes as visible in Eq. (16): in plane convection/diffusion and transport normal to the interface [160]. Since these processes are geometry-dependent [98,99], the time-dependency measured for these type of systems is due to transport phenomena, as opposed to being a true material parameter [3].

To make drop-shape analysis suitable for complex interfaces, one should (1) ensure that the measured quantity is indeed a material property, e.g. by repeating the measurement with different drop sizes, and (2) allow for anisotropic surface stresses, the occurrence of which is now well-established by different groups [48,109,161–167]. Estimating the surface stresses for complex interfaces can be aided greatly by including a measurement of the pressure inside the drop and obtaining the curvature locally, instead of a global fit of the Young–Laplace equation [48,166]. With the surface stresses known, iterative numerical procedures can be used to find the constitutive parameters of the interface, an approach generally called elastometry [48]. Alternatively, the constitutive equations can be applied directly to obtain the material parameters from the shape [103,164,167], which is a more straightforward, but seems to be a less accurate approach, as discussed in detail by Nagel et al. [48].

A closely related setup for measuring dilational properties of interfaces is the capillary pressure tensiometer (CPT), which combines a measurement of the radius of small drops, typically 10 to 100 $\mu$m, with a pressure measurement [168,169]. With the pressure inside the drop known, accurate measurements of the isotropic surface stress can be performed without the need for deformation due to gravity. In fact, smaller drops are preferred in the CPT, due to the higher signal to noise ratio of the pressure measurement, and the shorter capillary- and inertial relaxation times, allowing for measurements at higher frequencies [170]. In addition, the effect of shear becomes smaller for smaller drops, which have a shape closer to spherical [171], which can be exploited in the CPT to obtain interfacial deformations that are close to isotropic. As shown by the theoretical analysis by Kotula and Anna, the CPT can indeed be applied to complex interfaces in the presence of extra stresses [172]. Although the CPT is a large step forward in obtaining more isotropic deformations of interfaces, it can only be applied to interfaces of high curvature, due to the constraint of a spherical droplet shape.

Recently, a new experimental setup was proposed, called the radial through, which can apply truly isotropic deformations to a planar interface by moving an elastic band that is held in place by 12 “fingers” [58]. Due to the isotropic deformation, the stress state will be isotropic even for complex interfaces. This setup was later successfully applied to investigate surface viscoelasticity of a polymer multilayer at an air–water interface, and values were obtained that were consistent with
measurements using the rising bubble setup [109]. Moreover, it was shown for the first time that for these type of complex interfaces, concepts from bulk linear rheology, such as the Boltzmann superposition principle, indeed carry over to interfacial rheology (see Fig. 5). A miniaturized, 3D printable, version of the radial trough was developed by Kale et al., which allows for simultaneous dilatational deformation and interfacial microscopy [173].

6.3. Particle translating at a planar interface

Particles at complex interfaces are important for a variety of reasons. For example, they can be used to improve the stability of emulsions/foams [33], and the diffusion of particles at interfaces can give insights into the rheological properties of the interface [135,174]. Moreover, they can be used as idealized model system for understanding of, e.g. the diffusion of proteins in biomembranes [175]. In the limit of $B_4 \to \infty$, the hydrodynamic problem of a particle translating at a viscous interface in an unbounded domain is closely related to the Stokes’ paradox, which states that there is no creeping flow solution for a cylinder of infinite length translating perpendicular to its axis, which is due to the logarithmic decay of the disturbance velocity field [175,176]. Indeed, the slow decay of the velocity autocorrelation function leads to the inability of defining a surface viscosity, or diffusion coefficient, for such systems [177]. In the seminal work of Saffman and Delbrück, the logarithmic decay is cut short by including the subphases as “sinks for momentum”, and the mobility of a disk of radius $R$ at an incompressible, viscous planar interface of finite thickness is derived [178]. The solution given by Saffman and Delbrück is valid for $A = \eta R / \kappa_s \ll 1$, where $\eta$ is the bulk viscosity and $\kappa_s$ is the surface shear viscosity [179]. This model was later extended to all values of $A$ [180], and for finite depths of the subphase [179].

Although the assumption of surface incompressibility seems to hold for many types of interfaces, e.g. biomembranes, this assumption does not hold in general for interfaces with other types of surface-active moieties, see e.g. [58]. Moreover, particles protruding into the bulk phases might not be accurately approximated by a flat disk embedded in the interface. Danov et al. presented a numerical model for a spherical particle embedded in a planar interface with both effects from shear and dilation/compression present, but in the absence of Marangoni forces [181]. In a later work, effects from Marangoni forces were included up to first order, but without the coupling to flow in the bulk [182]. In the work of Fischer et al., a spheroid at an incompressible interface between two infinite bulk domains is considered [69]. They rationalize the surface incompressibility of the interface by assuming that the Marangoni effects are large. This, assumption, however, might break down for interfaces at low surface coverage, or with a weak slope with respect to $\Gamma$ in the equation of state $\sigma(\Gamma, T)$. A particle translating through an interface will under most circumstances generate a complex disturbance velocity field. This was assessed experimentally by using needles of different aspect ratios and a using broad range of relevant non-dimensional numbers ($Ma, B_4$ and the ratio between shear and dilatational $\eta_s / \kappa_s$) [183]. Drag coefficients for a probe in an incompressible interface are not expected to depend on probe aspect ratio, suggesting effects of compressibility or Marangoni stress related effects play a role. Elifring et al. investigated theoretically this interplay between interfacial rheology, Marangoni stresses and coupling with the bulk assuming a thin subphase, allowing for a lubrication approach [71], see Fig. 9. They reached the same conclusion that a particle translating at an interface is not always ideal for characterizing the shear rheological properties interfaces, due to the possible occurrence of a mixed flow field (dilation/compression and shear) and the tangled effects of Marangoni stresses and interfacial rheology. Methods with clean kinematics are recommended to determine interfacial shear and dilational properties, as outlined in the previous sections.

Since a full overview of the field of the hydrodynamics of particles at interfaces is beyond the scope of the current review, we will conclude this section by referring to two recent reviews for further reading [4,135].

6.4. Wrinkle analysis

We conclude this section with methods aimed at recovering the bending modulus of the interface, which are based typically based on the analysis of wrinkles occurring during compression. Wrinkling (also called “buckling”) occurs since, for low enough bending moduli, out-of-plane deformations can be a cheaper mode of deformation than in-plane compression. The resulting wave-length of the wrinkles can be used as a direct measure of the bending resistance of the interface. This analysis is typically done by assuming uniaxial compression of the interface, which allows for a 1D treatment, i.e. assuming invariance in the direction perpendicular to the compression, which is superimposed on a planar or curved shape. Starting point is the beam equation, which is given by [123]:

$$B \frac{\partial^4 h}{\partial x^4} + T \frac{\partial^2 h}{\partial x^2} + \Delta \rho g h = 0,$$

where $B$ is the bending modulus, $h$ is the vertical deflection of the interface, $T$ is the compressive force per unit length, $\Delta \rho$ is the density difference between the subphases and $g$ is the acceleration due to
are tested and calibrated in simple flows, as shown in the previous section, which can then be used to predict and benchmark the flow in increasingly complex flow scenarios. The latter is the topic of the current section of this review. For computational interfacial rheology, the complexity mainly arises due to the deformation of the interface, possibly leading to highly curved interfaces, thin fluid films and break-up and coalescence events. Since our focus is on continuum models, many of the numerical techniques available in the literature are based on the “classical” methods for bulk computational rheology, such as the finite difference method (FDM) [72], finite volume method (FVM) [190] and the finite element method (FEM) [42]. Moreover, the boundary element method (BEM), coupled to e.g. FDM or FEM for the surface computations, has been successfully applied as well [133,191].

7. Flows with deforming complex interfaces

The approach of computational interfacial rheology follows the same lines as computational bulk rheology [189]: constitutive models are tested and calibrated in simple flows, as shown in the previous.

7.1. Numerical approaches

Three main issues need to be addressed for the simulation of multiphase flows with deforming, rheologically complex interfaces: (1) describing the location of the interface, (2) evaluating the surface differential operators as introduced in Section 5 and (3) coupling the interfacial constitutive equation to the bulk flow. These issues are generally addressed by either interface capturing (IC) or interface tracking (IT) methods (see Fig. 10), which we will briefly review here.

In IC, the location is described in an implicit manner, typically by introducing a continuous function \( \phi = \phi(x,t) \), which is defined in the entire 3D domain, and the location of the interface is, by definition, the zero level set of this function: \( \phi(x) = 0 \). Assuming that \( \phi \) remains constant for a fixed material point yields in the Eulerian description:

\[
\frac{\partial \phi}{\partial t} + \mathbf{v} \cdot \nabla \phi = 0, \tag{44}
\]

which can be evaluated in the entire domain using standard methods. The normal to the surface can be obtained from \( \mathbf{n} = \nabla \phi / |\nabla \phi| \), which can in turn be used to evaluate the surface operations from the definitions \( \mathbf{I}_n = \mathbf{I} - \mathbf{n} \mathbf{n} \) and \( \mathbf{V}_n = \mathbf{V} \cdot \mathbf{n} \). Coupling to the bulk solution of, e.g. the velocity, can be done by approximating the interface with a small thickness, effectively converting the surface operations to volume operations, and using the model in the sharp-interface limit [192,193]. Alternatively, the interface can be reconstructed by a triangulation of the zero-levelset, and approaches similar to the extended finite element method (XFEM), where the solution space is enriched by allowing for discontinuities within elements, can be applied [194–196]. A major advantage of IC methods is that all equations can be solved on stationary Eulerian meshes, and that break-up and coalescence events are handled relatively easily, but they are generally less accurate than IT methods [197]. Variants of the IC method that have been used for interfaces with surface viscosity are the volume-of-fluid (VOF) method, where the phases are described by volume fraction in the cells [190], and phase-field/diffuse-interface methods, that typically have a sound physical basis to describe the interface with a finite thickness [193,198].

In the IT method, a surface mesh, i.e. a 2D mesh embedded in 3D space, is introduced that describes the interface. Both structured and unstructured 2D meshes, of varying interpolation order, have been used in the literature; a comprehensive overview is given by Barthès-Biesel [57]. The surface mesh is identified with the grid as introduced in Section 3, and the mesh velocity is thus identified with \( \mathbf{v}_g \). The normal velocity of the mesh is determined by Eq. (2), but the choice of the tangential velocity is arbitrary, which can be used to, e.g. make sure that the elements of the surface mesh remain evenly spaced and/or do not deform significantly [199]. Within the IT framework, evaluation of the surface differential operations is relatively straightforward due to the availability of the surface mesh, and can be done by e.g. identifying the curvilinear coordinates with the reference coordinates of the element as shown in Eqs. (37) and (38), and in Fig. 6. The coupling to the bulk depends on how the volume is discretized. Often, an “immersed boundary” approach is used, where the surface mesh is embedded in a stationary Eulerian grid, and forces are calculated in the nodes close to the interface, e.g. by using a smoothed delta function [72].

Fig. 9. Vector plot of the leading-order velocity field (a,c,e) and Marangoni flow field (b,d,f) overlaid on the leading-order concentration field (a,c,e) and concentration field perturbation (b,d,f). (a,b) Nearly inviscid interface \( B_q = 0 \), \( \theta = 1/\eta_c = 1 \); (c,f) low shear and large dilatational viscosity \( B_q = 0 \), \( \theta = 10 \); (e,f) large shear and no dilatational viscosity \( B_q = 10 \), \( \theta = 0 \).
This approach has the advantage that no boundary-fitted meshes have to be generated, but the solution close to the interface, i.e. within one volume element, is not accurate. Alternatively, meshes can be generated that are boundary fitted to the interface, such as the one shown in Fig. 10 (left), yielding very accurate solution close to the interface, but requiring regular remeshing [42]. Lastly, a combination between the FEM for the solution on the surface mesh and the BEM for the solution in the bulk has been proposed, with the advantage that the full flow field in the bulk is obtained, without the need for a volume mesh [133].

7.2. Drops and bubbles in shear flow

An important goal of computational interfacial rheology is the simulation of drops and bubbles, endowed with complex interfaces, in flow. Due to the coupling between the flow field, interfacial properties and transport equations, the governing equations allow for analytical solutions only under the simplest circumstances. For full 3D flows, large deformations and/or interactions between multiple drops and bubbles, numerical approaches are invaluable. Although simulations exist for drops and bubbles with complex interfaces in several flow scenarios, such as the oscillating pendant drop [42,116], freely rising bubbles [195] and Poiseuille flow [195,200], we will focus here on simple shear flow as it serves as a stepping stone for more complex flows.

The dynamics of drops and bubbles with rheological interfaces in simple shear flow can give insight into the bulk rheology and stability of emulsions and foams, and is therefore relevant from both fundamental and practical point of view. In addition, understanding the flow conditions for which breakup of drops/bubbles occurs is important for predicting, e.g. the droplet size distribution after processing of the material. Finally, the rheometric bulk flow conditions allow for comparisons to experiments on suspended drops with soft-matter interfaces [201,202], e.g. by investigating their equilibrium shape.

The transient dynamics of a single, isolated droplet depend on the shear rate and the material parameters of the drop, the suspending fluid and the interface. Generally, three scenarios are possible: the drop can (1) elongate and break up into smaller drops, (2) exhibit periodic deformations that can persist for long times or even indefinitely, or (3) attain a steady-state shape with the interface continuously moving around the drop in a process called “tank-treading” [203]. If a steady-state is reached, the drop typically takes on an ellipsoidal shape for smaller deformations, with the major axis tilted with respect to the shear flow direction, described by the inclination angle $\theta$. The deformation of the drop is quantified by the Taylor deformation parameter $D = (a - b)/(a + b)$, where $a$ and $b$ are the major and minor axes of the ellipse, respectively. For larger deformations, or for example in the case of confined shear flow, the steady-state shape of the drop significantly deviates from an ellipsoidal shape and it is often useful to use the length of the drop to quantify the amount of deformation [204].

As early as the 1950s, Oldroyd derived an expression for the viscosity of a dilute emulsion of spherical drops endowed with viscous interfaces [205]. This analysis was later extended by Danov to include the effects of Marangoni stresses and Gibbs elasticity [206]. The influence of surface viscosity on the deformation of an isolated drop in shear flow was investigated by Flumerfelt using a first-order perturbation analysis, valid for small deformations [207], and the first full numerical simulations were presented by Pozrikidis, which were, however, limited to surface viscosity ratios of unity [191]. A complete 3D numerical analysis of the steady state of drops with viscous interfaces, including the separate effects of shear and dilational viscosity, was presented by Gounley et al. who used the BEM, coupled to the FEM, to investigate the behavior of drops endowed with Boussinesq–Scriven interfaces in shear flow [133], see Fig. 11. Their analysis revealed that $D$ increases with surface shear viscosity, whereas it decreases with surface dilational viscosity. Since an increase in $D$ can lead to droplet breakup, this analysis can have implications for the stability of foams and emulsions during flow, e.g. material processing. Similar conclusion were reached by Luo et al., who investigated the coupled effect of a $H$-dependent surface viscosity and Marangoni stresses, assuming an insoluble surfactant [8]. They conclude that the coupling between surfactant transport, interfacial rheology and Marangoni stresses yield non-trivial and non-negligible alternations to the droplet dynamics.

Numerical simulations of droplets encapsulated by a (visco)elastic membrane in simple shear have been mainly motivated by research into biological systems, with the goal of mimicking e.g. red blood cells during flow. The systems under consideration can be broadly categorized as (1) vesicles, where the membrane consists of a “liquid-like” incompressible lipid bilayer with bending elasticity, (2) red blood cells, which are vesicles with an additional protein network attached to the bilayer to give it surface shear elasticity and (3) capsules, which is a generic term often used for droplets encased in a synthetic (e.g. polymer) compressible membrane [208]. Although biological systems are outside the scope of this review, the overlap with computational interfacial rheology is significant, so we will give a very brief overview here. More extensive reviews for the flow of vesicles and capsules are available in the literature [57,208].

In a series of papers [209–211], Pozrikidis and coworkers investigated the simulated capsules and vesicles in shear flow using a boundary element method (BEM) [212]. Following this work, different groups have successfully performed simulations of vesicles and capsules in shear flow using the BEM [68,213–218]. Moreover, other numerical methods have been proposed as well, such as the phase-field method [219], the level-set method [220], spectral BEM [221], boundary fitted FEM [222] and immersed boundary FEM [223,224]. The majority of the cited literature above focuses on either purely viscous or purely elastic membranes, whereas membrane viscoelasticity has received much less attention. Viscoelasticity of the membrane has been incorporated in simulations mainly by using the quasi-linear Kelvin–Voigt model as introduced in Section 4.4, thus by assuming that the surface...
stress is given by a superposition of a viscous surface stress, as given by the Boussinesq–Scriven model, and an appropriate hyperelastic surface stress. Diaz et al. used BEM simulations to investigate the behavior of a capsule with a viscoelastic membrane in an elongation flow [225]. The influence of membrane viscoelasticity of a capsule in shear flow was investigated by Yazdani and Bagchi [115]. A similar approach was taken by Gounley and Peng, using an immersed lattice Boltzmann method [226], which was also recently used for the simulation of red blood cells [227]. Benchmark solutions for a drop, endowed with a Boussinesq–Scriven or Kelvin–Voigt interface, in shear flow were presented by Carrozza et al. [228]. Carrozza et al. extensively validated their boundary-fitted FEM implementation using the method of manufactured solutions, and showed higher order spatial and temporal convergence.

Immersed FDM approaches that include viscoelastic membranes have been introduced recently by Li and Zhang [72,73]. In many of the above-mentioned works, it has been observed that a direct implementation of the Kelvin–Voigt model is unstable and therefore a standard linear solid (SLS) model is often used for the viscoelastic surface stress [72,115,226,227]. The SLS model can be interpreted as an elastic element in parallel with a viscoelastic Maxwell element, and thus by choosing the modulus in the Maxwell element large, the Kelvin–Voigt model is recovered. Finally, we note that particle-based method have been used as well for the simulation of viscoelastic membranes, where the membrane is modeled as a network of viscoelastic springs [229].

We conclude this section by briefly mentioning that capsules and vesicles in simple shear can exhibit buckling/wrinkling instabilities due to compressive stresses, similar to the buckling as introduced in Section 6.4. This phenomenon has been as observed experimentally [230] and in simulations [115,214], and more information on this topic can be found elsewhere [231].

7.3. Drainage and thinning flows

Drainage and thinning flows are important since they play a major role in the stability of emulsions and foams [46,232] and coating operations [233,234]. Due to the coupling between capillarity, transport phenomena and interfacial rheology, it is often difficult to predict drainage times for all but the simplest systems. Moreover, due to an inconsistent separation of material- and transport parameters, especially for area-changing flows, a clear link between stability and interfacial rheology has been established for only a limited number of systems, e.g. [33,235]. Numerical and analytical approaches are thus crucial in elucidating this complex problem. Often, drainage problems are understood in terms of mobility of the interface, which is a measure for the magnitude of the tangential surface velocity. An alternative interpretation, which is particularly useful for rheologically complex interfaces, is to consider the ability of the interface to “carry stress”, as expressed by Eq. (7). Interfaces with solely surface tension effects can also be “rigidified” by Marangoni stresses, as shown by Champougny et al. [233], and reproduced in Fig. 12. Since the films that are considered are generally much thinner than their lateral length scale, lubrication approaches can be applied which simplify the numerical methods considerably [1]. This approach allows for rewriting the governing equations in terms of the unknown height of the film, and by assuming radial symmetry, solutions can be sought on 1D meshes, often using simple FDM or FEM approaches.

The effect of interfacial viscosity and Marangoni stresses on the drainage between two drops was studied by Zapryanov et al., assuming the interface remained planar, thus the problem could be solved in a single point [236]. They concluded that, within the range of parameters included in their work, Marangoni stresses play a more important role in immobilizing the interface than interfacial rheology. Li studied the coalescence between two spherical bubbles being forced together, where the surface stress is given by the Boussinesq–Scriven model and a first-order effect of the Marangoni stresses is included [237]. Deformation of the interfaces was allowed, and dimples were observed, significantly altering the drainage behavior. Results were obtained that could explain experimental observation, but the analysis assumed no deviatoric stress inside the bubbles, and can thus not be extended to the drainage between drops. Chatzigiannakis and Vermant recently defined criteria how film rupture depends on the hydrodynamic conditions where a competition between the characteristic timescales of drainage and rupture has been experimentally determined [238,239]. Comprehensive numerical modeling is needed here that accounts for drop deformation dynamics, film drainage until the point of rupture including the random evolution of propagating fluctuations. Already for systems with a constant interfacial tension or surfactant transport this has been shown to be extremely challenging [240,241]. In a series of recent papers, the drainage between drops was studied by Ozan and Jakobsen, whose boundary integral approach does solve for the flow inside the drops [242]. They considered the coupled effect of surfactant transport, Marangoni stresses and a surface excess concentration-dependent surface viscosity [243]. Finally, they included non-linear surface viscoelasticity based on the SUCM model.

Fig. 11. Influence of surface viscosity on the deformation of droplets in simple shear flow. For both cases the viscosity ratio is λ = 1 and the capillary number Ca = 0.3. (a) Bq = 0 and (b) Bq = 10 and θ = 1 [133].

Source: Reproduced from [133] with permission from Cambridge University Press.

Fig. 12. Numerical results for the film thickness in a pulled soap film (Frankel configuration) as a function of capillary number Ca and Marangoni number Ma. The dashed line is the limiting case of a rigid interface, which is approached as Ma is increased, i.e. the interface is “rigidified”. See [233] for definitions of the symbols used here. Used with permission of Royal Society of Chemistry, from [233]; permission conveyed through Copyright Clearance Center, Inc.
Numerical analyses of other problems have been performed in a similar fashion. In the work of Hermans et al., a hemispherical dome was risen against into an air–water interface laden with different types of lung-surfactant replacements and the drainage of the film was investigated [54]. From numerical solutions of the drainage equation, which include the effects from both Marangoni stresses and surface rheology, experimental observations could be rationalized. Similar numerical approaches have been taken to describe the stability of antibubbles [244,245] and the classical Landau–Levich–Derjaguin (LLD) dip coating problem [234].

8. Open problems and outlook

From this review it is evident that quantitatively describing multiphase materials and in particular the role of a complex interface between the different components is a challenging task from both a computational and rheological point of view. Some of the challenges are quite similar as in the bulk flow of complex fluids; predictive constitutive models are essential that are valid not only in well-defined deformations such as shear, extension and compression/dilatation, but also in mixed flows. In this review several prototypical flows were discussed with a strong interplay between bulk flow and interfacial properties and despite all progress in literature, many challenges still need to be addressed. In particular, in systems where all length and time scales of bulk and interfaces are coupled and need to be resolved simultaneously. For example in drop–drop interaction up to five to six orders of magnitude in length scales are fully coupled and coalescence time scales are determined by the drainage of the liquid in the film, which is strongly dependent on interfacial transport and rheology. Even for well-designed smooth problems this is a very challenging (but also very relevant) problem to solve. Advanced computational methods that are accurate and efficient, such as full monolithic solvers, need to be developed for solving stiff numerical problems where all degrees of freedom are coupled. Also from a mathematical perspectives there are many open questions. Coupling different bulk and interfacial discretizations might give rise to (finite element) compatibility constraints and call might for stabilization techniques similar to the ones used to resolve the high Weissenberg number problem in bulk, such as the log-conformation approach [246,247]. Computational challenges also arise when interfacial phenomena or films reach a length scale well below those where continuum mechanics is still assumed to be valid. One could think of linking continuum bulk descriptions with molecular dynamics models for interfaces.

In addition to computational challenges also from a rheological point of view the scientific field is still wide open. For example in many industrial processes temperature plays an essential role which calls for experimental, theoretical and numerical methods to deal with temperature-dependent interfacial constitutive behavior. If coefficients in models, like a dilatational viscosity or modulus, are made temperature dependent one could argue if these type of constitutive relations are thermodynamically consistent. Other challenges are found when electrostatic charges become relevant or systems with a phase change across and at the interface. Also polymer crystallization at liquid–liquid interfaces is a process that simultaneously is influenced by interface chemistry and dynamics, and rheology.

To conclude, much progress has already been made in the field of computational interfacial rheology, but also many opportunities for further progress are present. An abundance in problems of both societal and industrial relevance could potentially benefit from this relatively young and exciting field, which offers a whole range of interesting numerical and theoretical challenges, waiting to be tackled.

Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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Appendix. Frame invariance of the surface upper convected derivative

We consider a frame rotation given by $Q(t)$, and denote quantities in the rotated frame with an asterisk, e.g. $n$ in the original frame becomes $n^*$ in the rotated frame. The rotation tensor $Q$ is orthogonal, thus $Q^T \cdot Q = I$. Proceeding in a similar manner as for the bulk [248], it can be verified that the following transformations are valid:

\begin{align}
I^*_s &= Q \cdot I_s \cdot Q^T, \\
\sigma^*_s &= Q \cdot \sigma_s \cdot Q^T, \\
\nabla^*_s &= Q \cdot \nabla_s, \\
L^*_s &= Q \cdot L_s \cdot Q^T + \Omega_s
\end{align}

where $I_s = (\nabla_s v_s)^T$ is the interfacial velocity gradient tensor and $\Omega_s = Q \cdot L_s \cdot Q^T$ describes the rate of rotation, where $(\cdot)$ has been used as a short-hand notation for the surface material derivative, i.e. the time derivative in a frame that translates with a surface particle. An alternative expression for the surface unit tensor in the rotated frame is $I^*_s = I^* - n^* n^*$. Using the relations given in Eqs. (45) to (49), and using symmetry of the surface stress tensor, it can be shown that

\begin{align}
\sigma^*_s - I^*_s \cdot \sigma_{ss} = \sigma_{ss} \cdot (L^*_s)^T \cdot Q^T &= Q \cdot (\sigma_s - I_s \cdot \sigma_s - \sigma_s \cdot L_s^T) \cdot Q^T, \\
\text{thus the surface upper convected derivative given in Eq. (26) is frame invariable. Likewise, it can be shown that}
\end{align}

\begin{align}
\sigma^*_s - I^*_s \cdot \sigma_{ss} = \sigma_{ss} \cdot (L^*_s)^T \cdot I^*_s \neq Q \cdot (\sigma_s - I_s \cdot \sigma_s - \sigma_s \cdot L_s^T \cdot I_s) \cdot Q^T.
\end{align}

which shows that the surface upper convected derivative appearing in, e.g. [53,107,117,118], is in fact not frame invariable.

References

[1] L. Gary Leal, Advanced Transport Phenomena, Cambridge University Press, 2007.
[2] J.C. Slattery, L. Sagis, E.-S. Oh, Interfacial Transport Phenomena, Springer Science+Business Media, LLC, 2007.
[3] G.G. Fuller, J. Vermant, Complex fluid-fluid interfaces: Rheology and structure, Annu. Rev. Chem. Biomol. Eng. 3 (1) (2012) 519-543.
[4] H. Manikantan, T.M. Squires, Surfactant dynamics: hidden variables controlling fluid flows, J. Fluid Mech. 892 (2020).
[5] M. Oettel, S. Dietrich, Colloidal interactions at fluid interfaces, Langmuir 24 (4) (2008) 1425-1441.
[6] A.J. Mendoza, E. Guzmán, F. Martínez-Pedrero, H. Ritacco, R.G. Rubio, F. Ortega, V.M. Starov, R. Miller, Particle laden fluid interfaces: dynamics and interfacial rheology, Adv. Colloid Interface Sci. 206 (2014) 303-319.
[7] B. Madivala, J. Fransaer, J. Vermant, Self-assembly and rheology of ellipsoidal particles at interfaces, Langmuir 25 (5) (2009) 2718–2728.
[8] Y.T. Luo, X.L. Shang, B.F. Bai, Influence of pressure-dependent surface viscosity on dynamics of surfactant-laden drops in shear flow, J. Fluid Mech. 858 (2019) 91-121.
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[38] W.B. Wong, M.A. Hulsen, P.D. Anderson, A numerical model for the development of the morphology of dispersed phases in complex flow, Rheol. Acta 58 (1-2) (2019) 79–95.

[39] H. Ritacco, F. Kiefer, D. Langevin, Lifetime of bubble rafts: Cooperativity and multiphase, Phys. Rev. Lett. 98 (2007) 1–4.

[40] J. Vermant, G. Ciocciolo, K. Golapan Nair, P. Moldenaers, Coalescence suppression in model immiscible polymer blends by nano-sized colloidal particles, Rheol. Acta 43 (5) (2004) 529–538.

[41] C. Huang, J. Forth, W. Wang, K. Hong, G.S. Smith, B.A. Helms, T.P. Russell, Bi-continuous structured liquids with sub-micrometre domains using nanoparticle surfactants, Nature Nanotechnol., 12 (11) (2017) 1060–1063.

[42] C. Balemanns, M.A. Hulsen, P.D. Anderson, Modeling of complex interfaces for pendant drop experiments, Rheol. Acta 55 (10) (2016) 801–822.

[43] C. Tanford, Ben Franklin Stilled the Waves: An Informal History of Pouring Oil on Water with Reflections on the Ups and Downs of Scientific Life in General, OUP Oxford, 2004.

[44] J. Krügel, S.R. Derkatch, Interfacial shear rheology, Curr. Opin. Colloid Interface Sci. 15 (4) (2010) 246–255.

[45] N.O. Jaensson, J. Vermant, Tensiometry and rheology of complex interfaces, Curr. Opin. Colloid Interface Sci. 37 (2018) 136–150.

[46] D. Renggli, A. Alicke, R.H. Ewaldt, J. Vermant, Operating windows for oscillatory interfacial shear rheology, J. Rheol. 64 (1) (2020) 141–160.

[47] M. Nagel, T.A. Tervoort, J. Vermant, From drop-shape analysis to stress-fitting elastometry, Adv. Colloid Interface Sci. 247 (2020) 33–51.

[48] J. Willard Gibbs, The Collected Works of J. Willard Gibbs. 1928, Longmans, New York, 1928.

[49] M. Schweizer, H.C. Öttinger, T. Savin, Nonequilibrium thermodynamics of an interface, Phys. Rev. E 93 (5) (2016) 1–8.

[50] H.C. Öttinger, D.C. Venerus, Thermodynamic approach to interfacial transport phenomena: Single-component systems, AIChE J. 60 (4) (2014) 1424–1433.

[51] D.C. Venerus, H.C. Öttinger, A Modern Course in Transport Phenomena, Cambridge University Press, 2018.

[52] A. Lamorgese, R. Mauri, L.M.C. Sagis, Modeling soft interface dominated systems: A comparison of phase field and Gibbs dividing surface models, Phys. Rev. Fluids 2 (2017) 1–54.

[53] E. Hermans, M.S. Bhamla, P. Kao, G.G. Fuller, J. Vermant, Lung surfactants and different contributions to thin film stability, Soft Matter 11 (41) (2015) 8037–8057.

[54] R. Hamed, D.M. Schenck, J. Fiegl, Surface rheological properties alter aerosol formation from mucus micromimetic surfaces, Soft Matter 16 (33) (2020) 7823–7834.

[55] S. Barman, M.L. Davidson, L.M. Walker, S.L. Anna, J.A. Zasadzinski, Inflammation product effects on dilatational mechanics can trigger the laplace instability and acute respiratory distress syndrome, Soft Matter 16 (29) (2020) 6890–6901.

[56] C. Wu, J.Y. Lim, G.G. Fuller, L. Cegelski, Quantitative analysis of amyloid-integrated biofilms formed by urapohagentic escherichia coli at the air-liquid interface, Biophys. J. 103 (3) (2012) 464–471.

[57] E.C. Hollenbeck, J.C.N. Fong, J.Y. Lim, F.H. Yildiz, G.G. Fuller, L. Cegelski, Molecular determinants of mechanical properties of v. cholerae biofilms at the air-liquid interface, Biophys. J. 107 (10) (2014) 2245–2252.

[58] P.A. Ruhs, L. Böcker, R.F. Inglis, P. Fischer, Studying bacterial hydrophobicity and biofilm formation at liquid-liquid interfaces through interfacial rheology and pendant drop tensiometry, Colloids Surfaces B 117 (2014) 174–184.

[59] Y. Summer Tein, Z. Zhang, N.J. Wagner, Competitive surface activity of monoclonal antibodies and nonionic surfactants at the air-water interface determined by interfacial rheology and neutron reflectometry, Langmuir 36 (27) (2020) 7814–7823.

[60] P. Matthew Spiecker, P.K. Kilpatrick, Interfacial rheology of petroleum asphaltenes at the oil-water interface, Langmuir 20 (10) (2004) 4022–4032.

[61] J.P. Kane, V. Paschard, A. Couzins, S. Banerjee, Interfacial rheology of asphaltenes at oil-water interfaces and interpretation of the equation of state, Langmuir 29 (15) (2013) 4750–4759.

[62] Z. Xue, A.J. Worthen, C. Da, A. Qajar, I. Robert Ketchum, S. Alzobaidi, C. Huh, M. Prodanovic`, K.P. Johnston, Ultradry carbon dioxide-in-water foams with viscoelastic aqueous phases, Langmuir 32 (1) (2016) 28–37.

[63] P. Van Pouvelde, S. Velankar, P. Moldenaers, Rheology and morphology of compatibilized polymer blends, Curr. Opin. Colloid Interface Sci. 6 (5-6) (2001) 457–463.

[64] L. Elias, F. Fenouillot, J. Majesté, Ph. Casanagni, Morphology and rheology of immiscible polymer blends filled with silica nanoparticles, Polymer 48 (20) (2007) 6029–6040.

[65] S. Vandebril, J. Vermant, P. Moldenaers, Efficiently suppressing coalescence in polymer blends using nanoparticles: role of interfacial rheology, Soft Matter 6 (14) (2010) 3353–3362.

[66] D. Langevin, Influence of interfacial rheology on foam and emulsion properties, Adv. Colloid Interface Sci. 88 (1-2) (2000) 209–222.

[67] H.A. Stone, S.A. Koehler, S. Higlendfeldt, M. Durand, Perspectives on foam drainage and the influence of interfacial rheology, J. Phys.: Condens. Matter. 15 (1) (2003) S283.

[68] N.B. Raikar, S.R. Bhata, M.F. Malone, D.J. McClements, C. Almeida-Rivera, P. Bongers, M.A. Henson, Prediction of emulsion drop size distributions with population balance equation models of multiple drop breakage, Colloids Surf. A: Physicochem. Eng. Aspects 113 (1-3) (2000) 141–1429.

[69] W.B. Wong, M.A. Hulsen, P.D. Anderson, A numerical model for the development of the morphology of dispersed phases in complex flow, Rheol. Acta 58 (1-2) (2019) 79–95.
[69] T.M. Fischer, P. Dhar, P. Heinig, The viscous drag of spheres and filaments moving in monolayers or multilayers, J. Fluid Mech. 558 (2006) 451–475.

[70] A. Ponce-Torres, J.M. Montanaro, M.A. Herrada, E.J. Vega, J.M. Vega, Influence of the surface viscosity on the breakup of a surfactant-laden drop, Phys. Rev. Lett. 118 (2) (2017) 1–5.

[71] G.J. Elfring, L.G. Leal, T.M. Squires, Surface viscosity and Marangoni stresses at surfactant laden interfaces, J. Fluid Mech. 792 (2016) 712–739.

[72] P. Li, J. Zhang, A finite difference method with subsampling for immersed boundary simulations of the capsule dynamics with viscoelastic membranes, Int. J. Numer. Methods Biomed. Eng. 35 (6) (2019) 1–22.

[73] P. Li, J. Zhang, Finite-difference and integral schemes for Maxwell visco stress calculation in immersed boundary simulations of viscoelastic membranes, Biomembr. Model. Membranobiol. (2020).

[74] J.M. Montanaro, A. Ponce-Torres, Review on the dynamics of isothermal liquid bridges, Appl. Mech. Rev. 72 (1) (2020) 1–29.

[75] P. Hansbo, M.G. Larson, Finite element modeling of a linear membrane shell equation for surfactant transport along a deforming interface, Phys. Fluids A 2 (1990) 111–112.

[76] C.J. Tucker, T.M. Squires, Surface shear inviscidity of soluble surfactants, Proc. R. Soc. Lond. A 413 (1987) 115–126.

[77] M.L. Kurnaz, D.K. Schwartz, Channel flow in a langmuir monolayer: Unusual velocity profiles in a liquid-crystalline mesophase, Phys. Rev. E 56 (3) (1997) 3778–3784.

[78] A.H. Sadoughi, J.M. Lopez, A.H. Hirs, Transition from Newtonian to non-Newtonian surface shear viscosity of phospholipid monolayers, Phys. Fluids 25 (3) (2013).

[79] P.T. Underhill, A.H. Hirs, J.M. Lopez, Modelling steady shear flows of Newtonian liquids with non-Newtonian interfaces, J. Fluid Mech. 814 (2017) 5–23.

[80] A. Raghunandan, A.H. Hirsa, J.M. Lopez, Predicting steady shear rheology of condensed-phase monomolecular films at the air-water interface, Phys. Rev. Lett. 121 (16) (2018) 164502.

[81] J. Hegemann, S. Knoche, M. Kott, S. Demand, A. Unverferth, H. Rehage, J. Kierfeld, Pendant capsule elasticity, J. Colloid Interface Sci. 513 (2018) 549–565.

[82] C.W. Macosko, Rheology: Principles, Measurements, and Applications, Wiley-VCH, New York, 1994.

[83] L.M.C. Sagis, Dynamic properties of interfaces in soft matter: Experiments and theory, Rev. Modern Phys. 83 (4) (2011) 1367–1403.

[84] R.B. Bird, R.C. Armstrong, O. Hassager, Dynamics of Polymeric Liquids. Vol. 1: Fluid Mechanics, Wiley-VCH, New York, 1987.

[85] M. Fornasier, M. Herty, R. Rascle, Nonlinear stability of discrete velocity Boltzmann models for incompressible viscous fluids, Commun. Math. Sci. 9 (3) (2011) 651–689.

[86] S. Liao, J. Neufeld, J. Nie, A. Yu, C. Balemans, M.A. Hulsen, T.A. Tervoort, C. De Michele, P. Ilg, Force and energy balance in discrete velocity Boltzmann models, J. Stat. Phys. 177 (2019) 920–953.

[87] B. Caleman, P.M. Vlahovska, D. Barthès-Biesel, C. Misbah, Flow dynamics of red blood cells and their biomimetic counterparts, C. R. Phys. 14 (6) (2013) 451–458.
