Vascular regrowth following photodynamic therapy in the chicken embryo chorioallantoic membrane

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Abstract Photodynamic therapy (PDT) induces damage to the endothelium, which can lead to increased vascular permeability and, under intensive PDT conditions, even to platelet aggregation, vasoconstriction, and blood flow stasis. Eventually, ischemia, hypoxia, and inflammation can occur, resulting in angiogenesis. We studied the sequence of the vascular events after Visudyne®-PDT in the chicken chorioallantoic membrane (CAM) at day 11 of development. Using epi-fluorescence microscopy, we monitored the regrowth of capillaries in the PDT treated area. Immediately after irradiation, the treatment resulted in blood flow arrest. And 24 h post PDT, sprouting of new blood vessels was observed at the edge of the PDT zone. Neovessels looping out from the edge of the PDT zone gave rise to specialized endothelial tip structures guiding the vessels towards the center of the treated area. At 48 h almost all of the treated area was repopulated with functional but morphologically altered vasculature. These observations also showed reperfusion of some of the vessels that had been closed by the PDT treatment. CAM samples were immunohistochemically stained for Ki-67 showing proliferation of endothelial cells in the PDT area. Also, several markers of immature and angiogenic blood vessels, such as αVβ3-integrin, vimentin and galectin-1, were found to be enhanced in the PDT area, while the endothelial maturation marker intercellular adhesion molecule (ICAM)-1 was found to be suppressed. These results demonstrate that the new vascular bed is formed by both neo-angiogenesis and reperfusion of existing vessels. Both the quantitative real-time RT–PCR profile and the response to pharmacological treatment with Avastin®, an inhibitor of angiogenesis, suggest that angiogenesis occurs after PDT. The observed molecular profiling results and the kinetics of gene regulation may enable optimizing combination therapies involving PDT for treatment of cancer and other diseases.

Keywords Photodynamic therapy · Capillary · VEGF · Angiogenesis · Real-time RT–PCR · Visudyne® · Avastin® · Galectin-1 · Vimentin

Introduction

Photodynamic therapy (PDT) is a minimally invasive treatment modality that can potentially destroy unwanted neoplastic tissue [1] while sparing neighbouring normal tissue. PDT involves site-specific activation of an administered photosensitizer using light of an appropriate wavelength, in order to generate cytotoxic reactive oxygen species that induce cellular and/or vascular damage, as well as inflammatory and angiogenic responses [2–4]. In the vasculature PDT can lead to cytoskeleton damage in the endothelium and endothelial cell retraction causing increased space between these cells. This can lead, when applied in patients, to exposure of the vascular basement membrane and the release of Von Willebrand factor, and, as a consequence to platelet activation and aggregation [2]. The effects of PDT in blood vessels, such as vessel constriction and stasis of flow shortly after phototherapy have been described by Star et al. [5]. They speculated that vascular damage plays an important role in tumor cure next to the direct effects of PDT on tumor...
cells. These findings are supported by the report of Henderson et al. [6] who quantified tumor cell clonogenicity at various times after PDT and found that the viability of tumor cells was nearly unaffected by PDT. Also, Selman et al. [7] demonstrated reductions in blood flow after phototherapy using a radioactive microsphere method. Reed et al. [8] studied vessel constriction using an intravital microscopy model and reported similar results. These studies identified platelet aggregation and vessel constriction as early events in PDT.

The angio-occlusive effect of PDT is currently used to treat non-cancerous vascular diseases. Prominent in this regard is the worldwide approval (in over 70 countries, including the USA) of verteporfin (Visudyne®)-based PDT for the treatment of exudative age-related macular degeneration (AMD), as well as for subfoveal choroidal neovascularization (CNV) due to pathologic myopia and ocular histoplasmosis syndrome [9]. A wide range of other diseases is under investigation for treatment with PDT using verteporfin or other PDT agents, including rheumatoid arthritis [10] and different forms of cancer [11, 12].

A suitable model for studying vascular effects of PDT is the well-vascularized chorioallantoic membrane (CAM) of the chicken embryo (Gallus gallus). This model has several advantages over other animal models, including the fact that the CAM consists of a thin, planar vascular network, which is well adapted to observation by microscopy [13]. Furthermore, the CAM provides an easily accessible neovascular network in a transparent matrix. It allows direct visualization of blood vessels before, during and after PDT, and during pharmacological intervention. The CAM has been successfully used to evaluate the photodynamically-induced vascular occlusion efficacy of some PDT photosensitizers, that are in clinical trials or are already FDA approved [14–17]. The CAM model has also been extensively used in angiogenesis research [18–20].

Research on the effect of PDT on the vasculature demonstrated that this treatment often results in the induction of angiogenesis, which is the major rationale for combining PDT with anti-angiogenesis therapy. The relationship between PDT and angiogenesis was first described by Ferrario et al. [21], who demonstrated that the effectiveness of PDT may be enhanced by combination with angiogenesis inhibitors, an approach that we also recently validated [14, 22]. In general, it was assumed that the PDT induced changes in the tissue result in the formation of new vasculature. This assumption was mainly based on the observation of the changed and tortuous appearance of the vasculature [14, 23, 24], but proof of neovascular formation by sprouting angiogenesis and vascular proliferation was not yet provided. Therefore, the present study was undertaken to investigate in the CAM some of the details of the mechanism of tissue revascularization after PDT. We show that neoangiogenesis occurs by observation of vessel morphology, by immunohistochemical detection of endothelial proliferation markers, and markers of angiogenesis (galectin-1 and vimentin), as well as by molecular profiling using real-time RT–PCR. We also suggest that next to new vessel formation, reperfusion of occluded blood vessels occurs. Understanding of the mechanisms of PDT-induced angiogenesis will help to optimize the improvement of PDT by combination with angiogenesis inhibitors.

Materials and methods

The in ovo CAM model

Fertilized chicken eggs (Animalco AG, Staufen, Switzerland) were labelled and transferred into a hatching incubator with a relative air humidity of 65% and a temperature of 37°C. This incubator was equipped with an automatic rotator (Savimat, Chauffry, France). On EDD 3, a hole of approximately 3 mm in diameter was opened in the eggshell and covered with a Laboratory Wrapping Film, Parafilm® (Pechiney, Menasha, USA) to prevent dehydration and possible infections. The eggs were then returned to the incubator in a static position until use. On embryo developmental day (EDD) 11, the hole in the shell above the air pouch of the egg is extended to a diameter of approximately 3 cm in order to provide better access to the chorioallantoic membrane for the experiments.

For the topical application of compounds, polyethylene rings were deposited on the CAM. These polyethylene rings (diameter 5 mm; wall thickness 0.5 mm, 1 mm height) confine the topical drug to only the small part of the CAM surface inside the ring. Eggs were placed under an epi-fluorescence microscope described below and PDT was performed. After the treatment the eggs were numbered, covered and returned to the incubator.

Microscopy and image acquisition

Microscopic observation of CAM vasculature and the light irradiation for PDT were performed with an epi-fluorescence Eclipse 600 FN microscope, as described previously [17, 25], equipped with a Plan Apo 4/0.2, working distance 20 objective (Nikon, Japan). Illumination was provided by a 100 W high pressure Hg-arc lamp. Light doses were adjusted with neutral density filters and measured with a calibrated Field-Master GS power meter (Coherent, Santa Clara, USA). For exciting and detecting Visudyne®, the microscope was equipped with a BV-2A filter set (\(\lambda_{\text{ex}} = 420 \pm 20 \text{ nm}, \lambda_{\text{em}} > 470 \text{ nm}, \text{ Nikon, Japan}\)). For detecting FITC, light was filtered for excitation at 470 ± 20 nm and a long-pass emission filter was used for detection of the

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fluorescence ($\lambda > 520$ nm, Nikon, Japan). Fluorescence images were acquired with an F-view II 12-bit monochrome Peltier-cooled digital CCD camera driven with analySIS DOCU software from Soft Imaging System (Muenster, Germany).

Visudyne®-Photodynamic therapy

This part of the study aimed at performing PDT to observe the evolution of the vascular network, especially in terms of vascular occlusion, during the 2 days following treatment. For this purpose, on EDD 11, the egg opening was extended to 3 cm in diameter, and a volume of 10 µl of Visudyne® (the liposomal formulation of verteporfin [26], Novartis Pharma, Inc., Hettlingen, Switzerland) was intravenously administered through a 33-gauge needle fitted to a 100 µl syringe (Hamilton, Reno, USA) into the main vessel of the CAM. This corresponds to 0.20 mg verteporfin per kg embryo weight. One minute after injection, the site with vessels of diameter between 5 and about 70 µm was irradiated with a light dose of 20 J/cm² ($\lambda_{ex} = 420$ nm, $\lambda_{em} > 470$ nm) with irradiance of 60 mW/cm². The irradiation area was 0.02 cm² as delimited by an optical diaphragm, within the area inside the polyethylene ring, which defined the area of possible topical drug administration. The site was photographed at the beginning and at the end of irradiation. Subsequently, the egg opening was sealed with parafilm and the embryo was further incubated for 24 h before assessing the PDT-induced damage. The conditions used here in the CAM model are the same as those that were previously selected in other studies [14]. They lead to similar angio-occlusion efficiency as observed after Visudyne®-PDT in the human eye at the most prevalent clinical conditions.

Optimal PDT-induced closure of vasculature in the CAM is defined as closing the same diameter as the choroidal neovessels (CNV) that are targeted in PDT in the case of wet age-related macular degeneration (i.e. < 70 µm in diameter), while leaving the larger vessels open. “Standard” clinical PDT of CNV conditions are a verteporfin dose of 6 mg/m² of body surface (0.15 mg/kg) and irradiation with 50 J/cm² at 689 nm, using an irradiance of 600 mW/cm², 15 min after the start of the slow 10-min infusion of the drug [27]. The transparency of the CAM allows using blue light (excitation at 420 nm) in order to excite the benzoporphyrin. In order to verify the efficacy of the blood flow stasis and the vascular occlusion induced by PDT under these conditions, observation of the vasculature was undertaken daily for the 2 days following the illumination by means of fluorescence angiographies. These were performed after i.v. injection of 20 µl of a solution containing of FITC-dextran (20 kDa, 25 mg/ml), followed by fluorescence angiography using light from an Hg-arc lamp filtered for excitation at 470 ± 20 nm and with a long-pass emission filter ($\lambda > 520$ nm) for observing the fluorescence. In order to increase the quality of the recorded angiographs, a light absorber, in the form of India ink, was injected (30 µl) into the extra-embryonic cavity just under the deposited polyethylene ring. The purpose of this second injection was to decrease the influence of the CAM autofluorescence background, which changes rapidly with time due to the embryo’s movement. The India ink was filtered using a sterile cellulose acetate membrane (0.2 µm pores, Renner GMBH, Darmstadt, Germany) just before injection. Between the treatment and this measurement, the eggs were again re-covered with parafilm, maintained in the dark and returned to the incubator.

In order to perform quantitative real-time RT–PCR experiments on the PDT effect, Visudyne®-PDT was performed on a large area of the CAM (0.5 cm²) at EDD 11. To that end, an Oxiius laser (Oxiius S.A., Lannion, France) was used, coupled to the frontal light distributor fiber, SN FD1-1351 (Medlight S.A., Ecublens, Switzerland) with an excitation wavelength of 405 nm (applied light dose of 20 J/cm² and the irradiance of 25 mW/cm²). After PDT, embryos were numbered, covered with parafilm and returned to the incubator. 48 h after PDT (EDD 13) the treated CAMs were fixed overnight in Zn-fixative solution, dried and frozen until the RNA extraction procedure.

Combining of Visudyne®-PDT with Avastin®

This part of the study was designed to observe the prolonged vascular occlusion, due to combination therapy consisting of photodynamic therapy followed by anti-angiogenesis. Experiments of Visudyne®-PDT were conducted as described above. Subsequently, 24 h post PDT, treated CAMs were i.v. injected with 20 µl of a solution containing FITC-dextran (20 kDa, 25 mg/ml), and observed by fluorescence angiography using light from an Hg-arc lamp filtered for excitation at 470 ± 20 nm and with a long-pass emission filter ($\lambda > 520$ nm). After that, Avastin® (bevacizumab), a product of Genentech, San Francisco, USA, was administered topically (20 µl, 1.7 mg/ml; 34 µg/embryo) in the polyethylene ring onto the CAM surface. In order to observe vascular regrowth after PDT under these conditions, observation of the vasculature was undertaken also 48 h post PDT by means of FITC-dextran fluorescence angiographies (as described above).

Immunohistochemistry

CAMs were fixed overnight in Zn-fixative [28] and embedded in paraffin. 4 µm sections were cut, dewaxed, and dehydrated. Endogenous peroxidase activity was blocked with 0.3% hydrogen peroxide in methanol for
30 min. Next, antigen retrieval was performed with a mixture of 2 M HCl and 0.2% Triton X-100 in tris buffered saline (TBS) for 30 min at room temperature, except for detection of smooth muscle actin (SMA). Slides were blocked with 10% normal goat serum and 1% BSA in PBS for 15 min, and subsequently incubated overnight with primary antibodies against Ki-67 (clone MIB-1, Dako, Glostrup, Denmark), αVβ3-integrin (clone LM609, Chemicon/Millipore, Amsterdam, The Netherlands), galectin-1 (rabbit polyclonal antibody, Peprotech, London, United Kingdom), vimentin (clone V9, Dako, Glostrup, Denmark), smooth muscle actin (SMA, clone 1A4, Dako, Glostrup, Denmark), and ICAM-1 (clone 166623, R&D Systems Europe Ltd., Abingdon, United Kingdom). Slides were washed three times with TBS between the antibody incubations. Visualisation was performed with either Power Vision poly-HRP kit (Immunologic, Duiven, The Netherlands) or EnVision + System-HRP kit (Dako, Glostrup, Denmark), only for smooth muscle actin and vimentin. This was followed by the development of the staining with 3,3'-Diaminobenzidine (DAB, Sigma Chemicals, The Netherlands) chromogenic substrate. Subsequently the slides were counterstained with haematoxylin, dehydrated and mounted in DePex mounting medium.

RNA isolation and cDNA synthesis

Total RNA was isolated from CAM sections using the RNeasy RNA isolation kit (Qiagen, Venlo, The Netherlands) according to the supplier’s protocol. Prior to column loading, samples were carefully homogenized in RLT buffer (Qiagen, Venlo, The Netherlands). Possible genomic DNA contaminations were removed by on column DNAse treatment with the RNase-free DNAse set (Qiagen, Venlo, The Netherlands) according to the supplier’s protocol. Prior to column loading, samples were carefully homogenized in RLT buffer (Qiagen, Venlo, The Netherlands). Possibly genomic DNA contaminations were removed by on column DNAseset (Qiagen, Venlo, The Netherlands). RNA quality and quantity were checked by spectrophotometry (NanoDrop, Thermo Scientific), and 1,000 ng RNA was used as input for first-strand cDNA synthesis using an iScript cDNA synthesis kit (Bio-Rad Laboratories, The Netherlands) and the manufacturer’s instructions. Reactions were diluted to 50 μl and stored at -20°C until use.

Primer design

Primers (Fig. 7) were targeted against beta-actin (Actin-β), cyclophilin-A (Cyclo-A), vascular endothelial growth factor A (VEGF-A), vascular endothelial growth factor receptors 1 and 2, (VEGFR-1, -R-2), neuropilin-2 (NRP-2), basic fibroblast growth factor (bFGF), integrin β3 (ITG-B3), galectin 1 (GAL-1) and vimentin (VIM). The primers were specific for chicken (Gallus gallus) sequences and selected based on the following requirements: (1) primer melting temperature of approximately 60°C, (2) GC content of approximately 55%, (3) preferably no G at the 5’ end, (4) avoid runs of more than three identical nucleotides, and (5) amplicon length of approximately 100 nucleotides. Specificity and cross-reactivity were checked with the Basic Local Alignment Search Tool (BLAST; http://www.ncbi.nlm.nih.gov/BLAST). All primers were synthesized by Sigma-Genosys, The Netherlands.

Quantitative real-time RT–PCR

Quantitative real-time RT–PCR (qRT–PCR) was performed in 25 μl reactions, containing 1× iQ SYBR Green supermix (Bio-Rad Laboratories, The Netherlands), 200 nM forward and reverse primer (Fig. 7c) and 1.5 μl cDNA. Reactions were run on a CFX96 thermal cycler (Bio-Rad Laboratories, The Netherlands), and consisted of an initial denaturation for 10 min at 95°C followed by 50 cycles of 15 s at 95°C and 1 min at 60°C. Following each run, melting curves were generated to verify specific product formation. Data were analysed using CFX Manager software (Bio-Rad Laboratories, The Netherlands) and the expression of each target gene was quantified relative to the expression of the reference genes (Actin-β and Cyclo-A) [29].

Results

Morphological characterization

The aim of this study was to investigate in detail some of the vascular events after Visudyne®-PDT. To that end, we performed PDT at the stage in which the CAM is already fully developed—EDD 11—and contains a vessel network with a regular capillary plexus (see Figs. 1a and 2a) [30]. We used previously optimized PDT protocols, which caused an almost total occlusion of the treated vessels [14]. Visudyne®-PDT caused thromboembolic events, and vascular constriction leading to obstruction of both large vessels and the capillary bed, which resulted in a complete perfusion arrest (see Fig. 1b and e). To evaluate the induction, and maintenance, of vascular occlusion after PDT, as well as to study the neovascularization and reperfusion processes, the treated area of the CAM was observed for 2 days post PDT. 48 h after Visudyne®-PDT a full revascularization had occurred (see Fig. 1c and f).

As has been previously described [14, 23], PDT causes the induction of inflammation and angiogenesis processes leading to development of a new functional vascular bed. After 24 h we observed that revascularization of the treated area starts by sprouting angiogenesis from existing vessel arches outside the treatment zone (see Fig. 2c and d, zone 1), into the angiogenic area. Cellular protrusions of
the leading edge tip cells can be seen (see Fig. 2b arrow I-III, and c arrow I). It is also observed that larger vessels (diameter 30–100 μm) that have been occluded by the PDT-induced thrombotic events get reperfused (see Fig. 2b and c, arrow IV), while newly developing small vessels (Fig. 2d, zone 2, arrow V) replace the original capillary plexus (like in zone 3).

After 48 h the area is repopulated with functional newly grown and reperfused vessels. This new vascular bed does not resemble the morphology of the original capillary plexus (see Fig. 2c and d, zone 3, in particular for vessels with diameter 3–5 μm), but instead, consists of larger vessels (see Figs. 2d, zone 2, and 1f, typically vessel diameter 5–30 μm) with a more tortuous morphology. Besides a different morphology, blood flow in these newly formed vessels is slow and inefficient, sometimes leading to halted or even reversed flow.

Histological characterization

In order to further investigate the fate and features of the vasculature after Visudyne®-PDT, histology was performed on Zn-fixed and paraffin embedded CAMs. Fig. 3a shows the gross histological appearance of the CAM 48 h after PDT over an area of 6.2 mm². This section is stained for smooth muscle actin to show the mature vasculature. As can be seen, the treatment induces wounding of the CAM tissue (the area between the indicated arrows, Fig. 3a) leading to a thinner membrane as compared to the untreated area. In panel B an equivalent part of the CAM is shown as an angiography, showing the differences in the vasculature between normal and PDT treated areas (Fig. 3b).

Immunohistochemical staining of the Ki-67 proliferation marker was performed, as well as detection of αVβ3-integrin as a marker of immature and angiogenic blood vessels. Ki-67 was found to be expressed in the vasculature, 48 h after PDT in the exposed area of the CAM (Fig. 4a). This result implies that new vasculature is formed by sprouting angiogenesis, requiring proliferation of endothelial cells. Moreover, we found expression of αVβ3-integrin in the vessels of the PDT treated CAM after 48 h, but not in the non-treated control areas (see Fig. 4b and c).

The previously identified markers of angiogenic blood vessels, vimentin [31] and galectin-1 [32], were detected in the CAM. Our data suggest that these markers are over-expressed in the newly formed vasculature in the PDT area as compared to the untreated area (Fig. 5). In addition, a molecule that is described as being suppressed in angiogenic endothelium [33] and serves more as a differentiation marker, i.e. ICAM-1, was found at lower levels of expression in the PDT area, as compared to the untreated CAM (Fig. 5). These data together demonstrate that the
vasculature contains angiogenically-activated blood vessels, and suggests that the formation of neovasculature occurs after application of PDT.

Evidence for a prominent role of the formation of new blood vessels in the CAM after PDT was further obtained by use of the well-known and clinically used angiogenesis inhibitor Avastin®. Although this anti-VEGF antibody was designed to bind human VEGF, a significant activity against chicken VEGF has also been reported [14]. Combination treatment of the CAM starting with Avastin® 24 h after PDT hours results in a considerable inhibition of the regrowth of the vasculature 48 h post PDT (Fig. 6d), as compared to the observations without Avastin® (Fig. 6b). This is in agreement with our previous findings [14].

Transcriptional expression of angiogenesis genes

To investigate and prove the induction and regulation of angiogenesis genes after PDT, we determined mRNA expression of a set of angiogenesis related genes, such as for VEGF-A, bFGF, VEGF receptors VEGFR-1 and -2, neuropillin-2, and endothelial angiogenesis markers, such as integrin β3, vimentin and galectin-1. RNA was isolated from control CAMs (EDD 11 and EDD 12), as well as from CAMs extracted 6 h (EDD 11), 24 h (EDD 12), or 48 h (EDD 13) after application of PDT. Expression of the tested genes did not differ significantly in the control groups (EDD 11 and EDD 12). These results were therefore all incorporated into a single control group. Fig. 7a–h show the relative transcriptional expression of the angiogenesis genes versus the reference genes beta-actin (Actin-ß) and Cyclophilin-A (Cyclo-A).

VEGF-A was observed to be significantly upregulated by approximately 2-fold immediately after PDT (6 h, Fig. 7a). Interestingly, this expression was normalized to control levels after 24 and stayed unchanged at 48 h. For bFGF a similar expression profile was found (Fig. 7b), indicating that angiogenesis is induced by a rapid spiking of activators, but that this signal is transient. A slower regulation is found for the VEGF receptors. VEGFR-1 and VEGFR-2 are both significantly induced by PDT as well. While their expression was found to be increased by factor of 13.5 (VEGFR-1) respectively a factor of 3 (VEGFR-2) at 24 h after PDT, the increase of this angiogenic environment remained at least

Fig. 2 Angiography images of the CAM after PDT visualized by FITC-dextran fluorescence angiography. a Normal (untreated) small vessels and capillary network, taken at EDD 13. b and c 24 h post PDT (EDD 12), whereas d was taken 40 h post PDT (EDD 12/13). Zones marked below pictures c and d represent: (1) non-regrown zones, (2) post PDT-regrown zone and (3) non-treated zone on the CAM. Phenomena of the regrowth process: (I) sprouting originating from the loop of pre-existing vessels, (II) dead-ended sprout, (III) filopodia with tip cell, (IV) recanalization of pre-existing, lumen-reduced vessels within PDT-treated area, (V) ongoing pillar building in neovascular meshes. In order to increase the contrast India ink was injected (30 l) into the extra-embryonic cavity right under the treated area. Image size: 1.4 × 1.12 mm (1,280 × 1,024 pixels with 4,095 grey levels)
until 48 h (Fig. 7c and d, respectively). Interestingly, the expression of another VEGF receptor, neuropillin-2 was already significantly upregulated 6 h after PDT, and peaked after 24 h. This receptor upregulation appears to be transient as well (Fig. 7e). We also tried to measure neuropillin-1, however this receptor was found not to be expressed at detectable levels.

The overexpression of integrin-β3 as well as of galectin-1 and vimentin as found by immunohistochemistry was confirmed by PCR analysis (Fig. 7f–h).

Discussion

The current work aimed at studying angiogenesis and neovascularization formation taking place after PDT, as well as the reperfusion of vessels occluded by PDT. Up to now, there was no consistent and firm proof in the literature that revascularization in the CAM after PDT involves neof ormation of vasculature. Several studies reported the observed altered vascular morphology, which is compatible with neo-angiogenesis, but proof of sprouting or vascular proliferation was not shown [14, 23, 24]. Here we present several lines of support for the contribution of sprouting angiogenesis after PDT in the chorioallantoic membrane (CAM) of the chicken embryo. We first showed that the process of sprouting angiogenesis and the presence of guiding tip-cells was readily observable by regular microscopy. Secondly, we found expression of Ki-67 in the vasculature of the PDT treated area by immunohistochemistry. Thirdly, we suggest overexpression of the endothelial angiogenesis markers αVβ3-integrin, vimentin and galectin-1, as well as suppression of the endothelial differentiation marker ICAM-1 within the PDT treated area at the protein level, 48 h post treatment. Fourthly, we demonstrated pharmacological suppression of revascularization by treatment with the anti-VEGF compound Avastin®. Lastly, molecular profiling by quantitative real-time RT-PCR demonstrated the spiking of the angiogenic growth factors VEGF and bFGF as well as the upregulation of VEGF receptors. In addition, the upregulation of the endothelial angiogenesis markers was confirmed at the transcriptional level.

We performed these studies in the CAM since this model has been used for studying and optimizing the effect of PDT on human choroidal (neo)vessels [16, 34–36]. The CAM has been used for studying the application of PDT for eye diseases, including exudative age-related macular degeneration. Although the application of PDT in some early stage cancers of the upper digestive tract, has been very successful [37, 38], in general applications for oncological diseases have been rather disappointing. Some of these applications can be simulated in the CAM after transplantation of tumor spheroids onto the membrane. The
The current study provides therefore also insights and tools for development of PDT for a number of diseases.

Our study, as well as earlier reports, supports the hypothesis that the CAM harbors an efficient vascular regeneration capacity similar to the human eye. After application of PDT, new vessels are formed to replace the original capillary plexus, a process, which is completed within 48 h (Fig. 2b and c). Larger blood vessels were also found to be occluded, but could be recanalized and/or reperfused. This is presumably possible because of the fact that larger vessels are more resistant to PDT-induced occlusion at the applied conditions. The latter observation is consistent with results published by Arroyo et al. [39]. However, it should be noted that we did not quantify the number or percentage of reperfused vessels versus newly formed vasculature in the PDT-treated area.

The architecture of the newly formed vessels is more tortuous and seems to be less organized when compared to the original capillary plexus. This observation is comparable to the tortuous morphology of vessels found in angiogenic tumors, a feature that can be partially changed by neutralization of VEGF [40], with antibody or antibody fragment against this protein. The architecture of tubular structures is determined by the sprouting of new tubes from preexisting ones. The tip cells respond to a gradient of VEGF-A by guided migration, while the proliferative response occurs in the sprout stalk [41]. We showed by PCR profiling that VEGF and VEGF receptors play a role in the PDT induced angiogenesis response. Interestingly, gene expression of both VEGF and bFGF is rapidly induced and already measurable after 6 h, indicative of the “explosive” angiogenic response to the PDT induced stress. After 24 and 48 h, the level of the angiogenic growth factors returns to control levels, but the pro-angiogenic condition is than maintained by enhanced expression of the growth factor receptors.

Previous studies in the CAM model have shown that exposure to different angiogenic stimuli, including VEGF and bFGF, resulted in increased angiogenic activity [42, 43], and that VEGF and bFGF exhibit a strong synergistic activity [44]. Induction of VEGF expression after PDT was also shown in several previous studies in the retinochioroidal area of the human eye [45, 46]. The induction of both bFGF and VEGF after PDT (6 h post PDT) was found by Schmidt-Erfurth et al. [27]. In this study immunohistopathologic examinations were performed on the eyes of patients who underwent enucleation after PDT. Also in oncological conditions PDT-induction of VEGF was shown. Uehara et al. showed that tumor cells exhibit a significantly higher VEGF expression 6 h after PDT than those of the untreated control groups [47, 48]. It is interesting to note that the kinetics and amplitude of the growth factor responses, that we found to be both rapid and transient in origin, seem to be identical in other systems. In the Uehara study, VEGF levels subsequently returned to control levels by 24 h after PDT. In another study by Chang et al. [49] VEGF up-regulation following PDT was monitored in the PC-3 prostate cancer model in immunodeficient mice. A statistically significant increase in VEGF was observed in PDT-treated tumors as early as 1 h post-PDT, reaching the highest value of 2.5-fold induction as compared to the control by 6 h post PDT.

Interestingly, also NRP-2, a transmembrane VEGF coreceptor, which is predominantly expressed in vein endothelial cells, in our studies also showed a rapid significant but rather transient upregulation 6–24 h after PDT. The other tested VEGF receptors, VEGFR-1 and VEGFR-2, were upregulated later (24 h after PDT), and stayed high at least up to 48 h.
The kinetics and levels of upregulation of these angiogenic stimuli post PDT will help to provide useful information on the optimization of the order and timing of anti-angiogenesis treatment when combined with PDT in order to enhance the therapeutic effects [50]. We have recently demonstrated improvement of PDT with ranibizumab, when applied 24 h after PDT [14]. Based on the PCR results obtained in the present study we expect an earlier VEGF response, suggesting that an earlier addition may be beneficial in the improvement of this combination therapy.

In order to find proof for neo-angiogenesis we also studied the expression of markers of angiogenic...
endothelium. First of all, we found overexpression of \( \alpha V \beta 3 \)-integrin, an activation marker on endothelium [51], in the PDT area of the CAM after 48 h. PCR analysis of the \( \beta 3 \) subunit of this integrin suggested confirmation of this response. Galectin-1 and vimentin were used as other activation markers. Galectins are a group of mammalian
beta-galactoside binding proteins with diverse functions that are not yet fully defined. It has been shown that galectins have intracellular regulatory roles in RNA splicing, act to inhibit or induce apoptosis, stimulate cell proliferation and differentiation, and regulate the cell cycle. Galectin-1 was previously found to function as the endothelial receptor for anginex, a novel peptide angiogenesis inhibitor [32]. In our study, galectin-1 expression was studied. Although not exclusively expressed in the vasculature, as is also the case in human and mouse tissues, we found galectin-1 to be slightly overexpressed in the newly formed vasculature in the PDT area as compared to the untreated area 24 h post treatment (Fig. 5). This finding was confirmed by PCR analysis.

Also vimentin was studied since it was reported to be overexpressed in angiogenic endothelium [31]. We found both at the protein and mRNA levels overexpression in the PDT area. Interestingly, vimentin cleavage has been reported in response to various inducers of apoptosis, such as ionizing radiation [52] and PDT [53]. Since vimentin is overexpressed in tumor endothelial cells [31], vimentin cleavage may be used as a diagnostic tool to assess therapeutic efficacy of PDT as well as apoptotic changes in certain tumors treated with PDT.

Collectively, our results demonstrate that PDT induces angiogenesis, involving among other growth factors, VEGF and VEGF signaling. It is also shown that the angiogenesis process resulting from Visudyne®-PDT involves both vascular neof ormation, as well as reperfusion of vessels, the former resulting in replacement of the capillary plexus, while the latter occurs in the larger blood vessels. The current results contribute to the possible further improvement of PDT results by optimizing the combination with angiogenesis inhibition. In particular the possibility of further optimization of the timing of the two therapeutic modes is indicated by the present results [54].

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