The Role of Anisotropy in Distinguishing Domination of Néel or Brownian Relaxation Contribution to Magnetic Inductive Heating: Orientations for Biomedical Applications

Luu Huu Nguyen 1,2,*, Pham Thanh Phong 1,2, Pham Hong Nam 3,4, Do Hung Manh 3,4,*, Nguyen Thi Kim Thanh 5,6,*, Le Duc Tung 5,6,* and Nguyen Xuan Phuc 7

1 Laboratory of Magnetism and Magnetic Materials, Advanced Institute of Materials Science, Ton Duc Thang University, Ho Chi Minh City 700000, Vietnam; phamthanhphong@tdtu.edu.vn
2 Faculty of Applied Sciences, Ton Duc Thang University, Ho Chi Minh City 700000, Vietnam
3 Institute of Materials Science, Vietnam Academy of Science and Technology, 18 Hoang Quoc Viet Street, Cau Giay District, Ha Noi 100000, Vietnam; namph.ims@gmail.com (P.H.N.); manhdh.ims@gmail.com (D.H.M.)
4 Graduate University of Science and Technology, 18 Hoang Quoc Viet Street, Cau Giay District, Ha Noi 100000, Vietnam
5 Biophysics Group, Department of Physics and Astronomy, University College London, Gower Street, London WC1E 6BT, UK
6 Healthcare Biomagnetic and Nanomaterials Laboratories, University College London, 21 Albemarle Street, London W1S 4BS, UK
7 Duy Tan University, K7/25 Quang Trung Street, Da Nang City 550000, Vietnam; phucnx1949@gmail.com
* Correspondence: luuhuunguyen@tdtu.edu.vn (L.H.N.); ntk.thanh@ucl.ac.uk (N.T.K.T.); t.le@ucl.ac.uk (L.D.T.)

Abstract: Magnetic inductive heating (MIH) has been a topic of great interest because of its potential applications, especially in biomedicine. In this paper, the parameters characteristic for magnetic inductive heating power including maximum specific loss power (SLP_{max}), optimal nanoparticle diameter (D_c) and its width (ΔD_c) are considered as being dependent on magnetic nanoparticle anisotropy (K). The calculated results suggest 3 different Néel-domination (N), overlapped Néel/Brownian (NB), and Brownian-domination (B) regions. The transition from NB- to B-region changes abruptly around critical anisotropy K_c. For magnetic nanoparticles with low K (K < K_c), the feature of SLP peaks is determined by a high value of D_c and small ΔD_c while those of the high K (K > K_c) are opposite. The decreases of the SLP_{max} when increasing polydispersity and viscosity are characterized by different rates of d(SLP_{max})/dr and d(SLP_{max})/dη depending on each domination region. The critical anisotropy K_c varies with the frequency of an alternating magnetic field. A possibility to improve heating power via increasing anisotropy is analyzed and deduced for Fe_3O_4 magnetic nanoparticles. For MIH application, the monodispersity requirement for magnetic nanoparticles in the B-region is less stringent, while materials in the N- and/or NB-regions are much more favorable in high viscous media. Experimental results on viscosity dependence of SLP for CoFe_2O_4 and MnFe_2O_4 ferrofluids are in good agreement with the calculations. These results indicated that magnetic nanoparticles in the N- and/or NB-regions are in general better for application in elevated viscosity media.

Keywords: magnetic heating; Néel & Brownian relaxation; particle anisotropy; polydispersity; ferrofluid viscosity

1. Introduction

MIH of magnetic nanoparticles (MNPs) while exposed to an alternating magnetic field (AFM) has attracted a lot of attention due to its potential applications in various domains, in particular cancer hyperthermia treatment and drug delivery. In cancer hyperthermia, it uses MIH on the principle that the cancer cells can be killed due to their higher thermal sensitivity than that of healthy ones [1–11]. For drug delivery, the MIH can be used to trigger remotely or on-site release of drug molecules being tagged to the MNPs [1–3,8,11–13].
Recently, new interesting biomedical applications were proposed including tuning the cellular gate for regulation of plasma glucose [14], biomaterials devitrification [15–17] and determination of MNPs accumulation in various organs [18]. In order to optimize the amount of MNPs used in the MIH, many studies focused on the conditions for maximizing heating efficiency, which is described theoretically by SLP or experimentally by specific absorption rate (SAR). The MIH power of MNPs has been known to consist of 3 main contributions: magnetization hysteresis, Néel relaxation generated by changing direction of the magnetic moments, and Brownian relaxation due to physical movement of MNPs. According to the linear response theory (LRT) [19,20], the Néel and Brownian relaxation processes are the main mechanisms to generate heat by the fluid containing superparamagnetic nanoparticles (NPs). Similar to other physical properties, the MIH power depends strongly on the diameter (D) of MNPs. Finding optimal particle diameter at which the SLP exhibits maximum value is frequently the purpose of both theoretical and experimental MNPs-MIH research.

Theoretical calculations indicated that, as a result of the competition between Néel and Brownian dissipation processes, the SLP versus D curve exhibits a peak shape with maximum value (SLP max) at a characteristic particle diameter Dc for different material parameters and field conditions [21–26]. From the studies of various Fe3O4 (FO) MNPs with different size at frequency f = 376 kHz, the maximum SLP max was found for a 16 nm (size standard deviation, σ = 0.175) sample [27–29]; for iron oxide nanocubes at f = 520 kHz, it is 19 ± 3 nm [30,31]. An analysis of various data after taking a normalization of field factor gave an elevation of SLP in the diameter range from 14–18 nm [25]. For γ-Fe2O3, elevation of SLP for 5 sample sizes from 5.3 nm to 16.5 nm (σ = 0.19–0.43) is in agreement with the theoretical prediction for the peak appearance at Dc = 14.5 nm [22]. Although these results have confirmed the existence of optimal particle size Dc of MNPs in MIH, finding the value of Dc is not a simple task in experimental works because of the impact of other parameters such as the magnetic anisotropy, viscosity of fluid, and the size distribution.

Firstly, while the magnetic anisotropy of MNPs can be considered as a constant in theoretical works, it depends strongly on the particle size. Additionally, it was showed that the SLP max and Dc decreases monotonically with increasing anisotropy [23,24]. It is noted that, due to the difference in morphology, the synthesized MNPs of the same material can have quite different polydispersity, anisotropy K values (e.g., FO MNPs having K ranging from about 20 to 550 kJ/m3 [32,33]) which can influence the SLP max and Dc parameters. Secondly, the value of SLP max was found to reduce with expansion of size distribution [22]. In practice, there will be some size distribution of the MNPs regardless of the synthesis method and producing MNPs with a sufficiently narrow size distribution is a difficult task. Thus far there have been few reports on experimental verification of calculated optimal D which would require the ability to synthesize MNPs with high monodispersity and to tune D precisely [22,25,28,34]. Thirdly, there might be some relationships between the value of Dc and SAR and ferrofluid viscosity. The size dependences of heating power with some variations of D and ferrofluid viscosity was studied experimentally and theoretically which showed for example for γ-Fe2O3 and CoFe2O4 MNPs SAR decreased about 20% and 80% with an increase of the viscosity, respectively [22]. To be able to obtain MNPs with optimal heating power, it is desirable to develop a complete correlation of SLP versus D and to consider impacts of different parameters, e.g., size distribution and shape of the NPs [20–22].

In this work, assessments of the impact of K on overall behavior of the heating power quantity have been systematically analyzed. The characteristics of SLP versus D for different MNPs have been studied by considering the impacts of two experimental parameters of the MNPs ferrofluid: σ and media viscosity (η). The different shapes of SLP(D) or the different rates of d(SLP max)/dσ and d(SLP max)/dη for FO MNPs with various anisotropy have been studied and explained as a result of the competition between Néel and Brownian dissipation processes. Here, the experimental results of MNPs of manganese ferrite (MFO), and cobalt ferrite (CFO) are considered as representative of low K (Néel
domination) N type, and high K (Brownian domination) B type, which have confirmed the theoretical predictions.

2. Theoretical Basis

The SLP of the MNPs can be calculated as follows [4,20–26]:

\[
\text{SLP} = \frac{P}{\Phi \rho},
\]

(1)

where \( \Phi \) is the volume fraction (%), \( \rho \) the mean mass density (g/m\(^3\)) and \( P \) the loss power density (W/m\(^3\)). The calculations were carried out for particles with size standard deviation (or size polydispersity) parameter \( \sigma = 0\text{–}0.5 \), and viscosity \( \eta = 1\text{–}10 \text{ mPa·s} \), assuming the volume fraction \( \Phi = 0.1\% \) and the surface ligand layer thickness of 1 nm.

For the superparamagnetic NPs, it is generally known that Néel and Brownian relaxation losses mainly contribute to the MIH of materials. The Néel relaxation loss is originated from relaxation effects of magnetization in a magnetic field, the Brownian relaxation loss is due to the rotation of the NPs as a whole in a ferrofluid. In the LRT, \( \chi \) is assumed to remain constant with increasing \( H \). This approach was shown to be valid for small magnetic fields. Based on theoretical results, it was found that the condition of validity for the LRT is \( \chi < 1 \). The dimensionless parameter, \( \xi \), can be given by ref. [19]:

\[
\xi = \frac{\mu_0 M_s V H}{k_B T},
\]

(2)

Therefore, LRT based on Néel and Brownian relaxation losses is suitable for superparamagnetic NPs or \( H << H_C \) [19]. The correlation between SLP (based on LRT), the field amplitude (\( H \)), frequency (\( f \)) and the MNPs imaginary susceptibility (\( \chi'' \)) is ref. [20,24]:

\[
\text{SLP} = \pi \mu_0 \chi'' H^2 f,
\]

(3)

with \( \mu_0 \) being the permeability of free space; where

\[
\chi''(f) = \chi_0 \frac{f \tau}{1 + (f \tau)^2},
\]

(4)

The effective relaxation time (\( \tau \)) can be determined from the compositional relaxation of Néel (\( \tau_N \)) and Brownian (\( \tau_B \)) processes [20,24]:

\[
\tau = \tau_N \tau_B / (\tau_N + \tau_B),
\]

(5)

with

\[
\tau_N = \frac{\sqrt{\pi}}{2} \tau_0 \exp(KV/k_B T) \sqrt{KV/k_B T},
\]

(6)

\[
\tau_B = \frac{3 \eta V H}{k_B T},
\]

(7)

where \( V \) and \( V_H \) are the volume of the core magnetic, and the whole capped particle, respectively.

For monodisperse superparamagnetic NPs (\( \sigma = 0 \)), the value of SLP is calculated based on above equations. Considering the impact of particle size deviation (\( \sigma > 0 \)), the mean loss power density can be described as ref. [20]:

\[
P = \int_{0}^{\infty} P_g(D) dD,
\]

(8)
with
\[ g(D) = \frac{1}{\sqrt{2\pi}\sigma D} \exp \left[ -\frac{(\ln(D/D_0))^2}{2\sigma^2} \right], \tag{9} \]
and \( g(D) \) the distribution function
\[ \int_0^\infty g(D)dD = 1, \tag{10} \]

3. Results and Discussion
3.1. Characteristics of Optimal Parameters in Domination Regions of Néel or Brownian Relaxations

Magnetite is one of the extensively studied and important in a wide range of medical applications because of its biocompatibility. The anisotropy value of FO MNPs was reported between a few tens to higher than 500 kJ/m³ \([32,33]\). The calculations are, therefore, made for different \( K \) up to 50 kJ/m³ and the results of SLP versus particle diameter at \( K \) equal to 9 kJ/m³, 20 kJ/m³, 41 kJ/m³ are presented in Figure 1.

![Figure 1. SLP versus D, calculated at f = 100 kHz, H = 5.18 kA/m, \( \sigma = 0, \eta = 1 \) mPa·s for monodisperse FO MNPs with 3 different \( K \) of 9, 20, and 41 kJ/m³. The bars denote the (full-width-half-maximum (FWHM)) \( \Delta D_c \).](image)

The typical peak behaviors of the calculated SLP against D obtained for FO MNPs can be seen in Figure 1. Here, the difference in the SLP (D) graph shape of FO MNPs depends on the value of \( K \) \([20,23]\). We have introduced full-width-half-maximum (FWHM) \( \Delta D_c \) for describing the peaks. The \( D_c, \Delta D_c \) and SLP_{\text{max}} obtained at \( f = 100 \) kHz, \( H = 5.18 \) kA/m (65 Oe), \( \sigma = 0, \eta = 1 \) mPa·s for monodisperse FO ferrofluids with different anisotropy \( K \) are listed in Table 1.

The results showed that the high \( K \) (50 kJ/m³) FO sample (18.5 nm) has much smaller value of \( D_c \) compared with that of the low \( K \) (3 kJ/m³) one (28.5 nm). In contrast, there is a large increase in the value of FWHM \( \Delta D_c \) when the value of \( K \) goes from 3 kJ/m³ (3.5 nm) to 50 kJ/m³ (16.5 nm). The fact that the SLP peak is narrow for low \( K \) but broad for high \( K \) can be attributed to Néel or Brownian domination, respectively \([9,20,22,24]\).

Based on Equation (5), it is clear that the effective relaxation time is dominated by the shorter of the two components. For example, A. E. Deatsch et al. found that the Brownian relaxation becomes more significant at 13 nm for high anisotropy particles (40 kJ/m³) \([25]\). We calculated the value of relaxation times at \( D_c \) for all samples. As can be seen in Table 1, the value of effective relaxation time is approximately equal to the Brownian relaxation...
time at $D_c$ when the value of $K$ is higher than 19 kJ/m$^3$. The calculations indicated that the Brownian relaxation dominated at $D_c$ when the value of $K$ is higher than 19 kJ/m$^3$. Therefore, the difference in peak behaviors of the SLP against $D$ depends on the domination of Néel or Brownian relaxations. As can be seen in Table 1, the value of $D_c$ changes with an increase of $K$ from 3 kJ/m$^3$ to 20 kJ/m$^3$, because the Néel relaxation loss still affects this parameter. When the value of $K$ for FO is higher than 20 kJ/m$^3$, $D_c$ and SLP$_{max}$ are unchanged due to the domination of Brownian relaxation loss. Therefore, it changes abruptly at some critical anisotropy $K_c = 20$ kJ/m$^3$.

Table 1. $D_c$, $\Delta D_c$, SLP$_{max}$, $\tau_N$, $\tau_B$, and $\tau$ obtained for monodisperse FO ferrofluids with different anisotropy constant $K$. ($f = 100$ kHz, $H = 5.18$ kA/m, $\sigma = 0$, $\eta = 1$ mPa·s).

| $K$ (kJ/m$^3$) | $D_c$ (nm) | $\Delta D_c$ (nm) | SLP$_{max}$ (W/g) | $\tau_N$ (s) | $\tau_B$ (s) | $\tau$ (s) |
|----------------|-------------|-------------------|-------------------|----------------|-------------|-------------|
| 3              | 28.5        | 3.5               | 76.9              | $1.95 \times 10^{-6}$ | $10.77 \times 10^{-6}$ | $1.65 \times 10^{-6}$ |
| 5              | 24          | 3                 | 71.4              | $1.87 \times 10^{-6}$ | $6.67 \times 10^{-6}$ | $1.47 \times 10^{-6}$ |
| 7              | 21.5        | 4                 | 66.2              | $1.98 \times 10^{-6}$ | $4.92 \times 10^{-6}$ | $1.42 \times 10^{-6}$ |
| 9              | 20          | 6.5               | 62.3              | $2.65 \times 10^{-6}$ | $4 \times 10^{-6}$ | $1.6 \times 10^{-6}$ |
| 12             | 18.5        | 9.5               | 58.3              | $4.26 \times 10^{-6}$ | $3.27 \times 10^{-6}$ | $1.85 \times 10^{-6}$ |
| 15             | 17.5        | 12.5              | 50.9              | $3.24 \times 10^{-6}$ | $2.81 \times 10^{-6}$ | $2.02 \times 10^{-6}$ |
| 19             | 17          | 14                | 46.9              | $3.46 \times 10^{-6}$ | $2.6 \times 10^{-6}$ | $1.52 \times 10^{-6}$ |
| 20             | 17          | 14.5              | 45.9              | $2 \times 10^{-3}$ | $2.6 \times 10^{-6}$ | $2.6 \times 10^{-6}$ |
| 21             | 18.5        | 14.5              | 43.6              | $4 \times 10^{-3}$ | $3.27 \times 10^{-6}$ | $3.27 \times 10^{-6}$ |
| 30             | 18.5        | 15                | 43.6              | $4.903$           | $3.27 \times 10^{-6}$ | $3.27 \times 10^{-6}$ |
| 41             | 18.5        | 16                | 43.6              | $2.8 \times 10^{5}$ | $3.27 \times 10^{-6}$ | $3.27 \times 10^{-6}$ |
| 50             | 18.5        | 16.5              | 43.6              | $3.4 \times 10^{7}$ | $3.27 \times 10^{-6}$ | $3.27 \times 10^{-6}$ |

Changes of characteristic parameters, SLP$_{max}$, $D_c$ and $\Delta D_c$ as a function of $K$ for $f = 100$ kHz, $\eta = 1$ mPa·s are presented in Figure 2, where it suggests 3 different regions. In the lowest $K$ (region I: $K \leq 5$ kJ/m$^3$): SLP$_{max}$, $D_c$ and $\Delta D_c$ decrease with increasing $K$. The middle region (region II: $5$ kJ/m$^3 \leq K \leq 20$ kJ/m$^3$) is characterized by a tendency of the decrease of $D_c$ to slow down while $\Delta D_c$ starts to increase with increasing $K$. In the high $K$ region (region III: $K > 20$ kJ/m$^3$), all the 3 parameters become almost constant. Relating to the dissipation mechanisms, the regions I, II and III can be correspondingly assigned as Néel-domination (N-region), Néel/Brownian overlap (NB-region) and Brownian-domination (B-region). While the transition from N- to NB-region is quite smooth, the transition to the B region is distinctly of the first order and in case of FO MNPs it corresponds to a critical anisotropy value $K_c$ of about 20 kJ/m$^3$.

![Figure 2](image-url)
3.2. Dependence of Critical Anisotropy $K_c$ on Frequency ($f$)

Based on LRT, the value of SLP reaches the maximum $SLP_{\text{max}}$ at the optimal particle size $D_c$ when the condition $\omega\tau = 1$ is satisfied. Therefore, the anisotropy boundary of the transition from NB- to B-region might depend on the frequency of AMF.

Based on the data of FO MNPs at $\eta = 1$ mPa·s for the expanded $K$ range and at various frequencies, the SLP was calculated and results of $D_c$ versus $K$ are presented in Figure S1a. For frequencies up to 1000 kHz can be seen an abrupt change of $D_c$ at $K_c$ associated with the transition to the Brownian domination region (for example with $f = 500$ kHz, the value of $K_c$ is about 60 kJ/m$^3$, and the three N, NB and B regions are presented in Figure S1b. The dependence of the critical anisotropy $K_c$ on the field frequency is presented in Figure 3, which follows the function:

$$K_c(f) = A \left(1 - e^{-B(f-f_0)}\right),$$  \hspace{1cm} (11)

where $A = 214.63$ kJ/m$^3$, $B = 0.0000814$ ms, and $f_0 = 81.27$ kHz are fitting constants.

The values of critical anisotropy $K_c$ at different frequencies for fluids with various viscosities are listed in Table 2. For MFO fluid with $K = 3$ kJ/m$^3$, the Brownian relaxation dominates when $\eta = 1$ mPa·s and $f = 100$ kHz (low frequency) but it becomes the Néel relaxation domination when $\eta \geq 1$ mPa·s or $f \geq 100$ kHz. For CFO fluid, the Néel relaxation dominates when $\eta \geq 4$ mPa·s or $f \geq 500$ kHz, but it is the Brownian relaxation domination when $\eta \leq 2$ mPa·s or $f \leq 1000$ kHz.

| $f$ (kHz) | $K_c$ (kJ/m$^3$) | $\eta = 1$ | $\eta = 2$ | $\eta = 4$ | $\eta = 6$ | $\eta = 8$ |
|----------|-----------------|----------|----------|----------|----------|----------|
| 100      | 20              | 33       | 60       | 83       | 102      |
| 200      | 31              | 56       | 103      | 147      | 205      |
| 300      | 41              | 74       | 141      | 207      | 261      |
| 400      | 51              | 95       | 188      | 252      | 322      |
| 500      | 59              | 112      | 227      | 308      | 399      |
| 750      | 100             | 153      | 292      | >400     | >400     |
| 1000     | 102             | 205      | 364      | >400     | >400     |

Figure 3. $K_c$ versus $f$ at $\eta = 1$ mPa·s, the fitting gave $R^2 = 0.94121$. 

The values of critical anisotropy $K_c$ at different frequencies for fluids with various viscosities are listed in Table 2. For MFO fluid with $K = 3$ kJ/m$^3$, the Brownian relaxation dominates when $\eta = 1$ mPa·s and $f = 100$ kHz (low frequency) but it becomes the Néel relaxation domination when $\eta \geq 1$ mPa·s or $f \geq 100$ kHz. For CFO fluid, the Néel relaxation dominates when $\eta \geq 4$ mPa·s or $f \geq 500$ kHz, but it is the Brownian relaxation domination when $\eta \leq 2$ mPa·s or $f \leq 1000$ kHz.

Table 2. Values of $K_c$ at different frequencies for fluids with various viscosities ($\eta$ (mPa·s)).
3.3. Orientations to Choose Proper Regions in Biomedical Applications

For biomedical applications, the size distribution and the viscosity of ferrofluid must be considered. In the above calculation of the relaxation times and MIH power of MNPs, the particles were assumed to have the same size, in other words the MNPs are monodisperse with $\sigma = 0$. However, in reality, this assumption cannot be satisfied because usually there would exist some size distribution of the NPs regardless of the synthetic method used. In practice, producing monodisperse MNPs ($\sigma = 0$) is almost impossible task. For example, J. P. Fortin et al. synthesized 16.5 nm $\gamma$-Fe$_2$O$_3$ with $\sigma = 0.43$, which could be reduced to 0.19 (d = 5.3 nm) after size sorting by successive phase separations [22]. M.P. Pileni et al. synthesized 2–5 nm CoFe$_2$O$_4$ with 30% polydispersity in size distribution by using functionalized surfactants [35]. When A. K. Gupta et al. compared the different characteristic features of the iron oxide NPs fabricated through different methods, they were always polydisperse NPs with narrow or broad size distributions [3]. Therefore, the assumption ($\sigma = 0$) appears not to be realized. In fact, in the synthesis of MNPs using seed mediated-growth or size sorting route, the common value of $\sigma$ was reported in between 0.3–0.5 but sometime it can reduce to 0.15–0.2 [22, 36, 37]. The polydispersity characterized by the $\sigma$ of MNPs can give rise to the reduction of SLP [20]. For $\gamma$-Fe$_2$O$_3$ MNPs, $\sigma$ in the range of 0.08–0.15 could result in a decrease of SLP$_{\text{max}}$ to half of the monodisperse value [22, 24]. Calculations were carried out for various anisotropy (K) and standard deviation ($\sigma$) of FO MNPs at $f = 100$ kHz, $H = 5.18$ kA/m, $\eta = 1$ mPa·s and the results of relative SLP$_{\text{max}}(\sigma)/$SLP$_{\text{max}}(\sigma = 0)$ are represented in Figure 4.

![Figure 4](image_url)

Figure 4. SLP$_{\text{max}}(\sigma)/$SLP$_{\text{max}}(\sigma = 0)$ calculated at $f = 100$ kHz, $H = 5.18$ kA/m, $\eta = 1$ mPa·s for FO samples with $K = 9, 20$, and 41 kJ/m$^3$.

The change of heating power behavior with varying $K$ has been reflected clearly also in the dependence of relative SLP on size standard variation. It can be seen that the domination region strongly influences the behavior of SLP besides material composition and particle size. Our results in Figure 4 indicate that, in all the curves, the SLP$_{\text{max}}$ decreases with increasing $\sigma$ and there is a clear trend of increasing relative SLP$_{\text{max}}$ when the value of $K$ changes from the NB-region (9 kJ/m$^3$) to $K_c$ (20 kJ/m$^3$) and then the B-region (41 kJ/m$^3$). In other words, for the similar polydispersity degree $\sigma$, the MNPs in the B-region would have higher heating power than that of those in the NB-region. These results indicated that the monodispersity requirement for getting the same heating power is much less strict for the MNPs in B-region as compared with the case of MNPs in N- or NB-region. Quantitatively, the polydispersity-caused SLP reduction for iso-dispersity of $\sigma = 0.2$ FO MNPs and $\sigma_{50}$ (defined as at the position of $\frac{1}{2}$ SLP$_{\text{max}}$) with various anisotropies at $f = 100$ kHz, $H = 5.18$ kA/m, $\eta = 1$ mPa·s are listed in Table 3. The parameter $\sigma_{50}$ is seen to increase from 0.21 to 0.58 with $K$ from 9 to 32 kJ/m$^3$, then becomes constant for $K \geq$...
indicating that the monodispersity requirement for obtaining the same heating power is much less strict for the high K as compared with the case of low K MNPs. The results in Table 3 also show that the polydispersity-caused SLP reduction decreased with an increase of magnetic anisotropy. From the slope of the SLP graph in Figure S2, it is estimated that an increase of K by about 4 times can result in saving as much as 35% of the heating power. These results seem to be consistent with the observation on cubic-shaped FO MNPs of about 20 nm (K = 180 kJ/m$^3$) having higher heating power than spherical ones (K = 20 kJ/m$^3$) [32]. The improvement of heating power by increasing K is an interesting topic and it has been recently reported for different materials, while the elevation of K was possible by various approaches including surface morphology, exchange-bias or stacking of particles in chains [32,33,36–39].

| K (kJ/m$^3$) | SLP Reduction (%) | $\sigma_{50}$ |
|-------------|-------------------|--------------|
| 9           | 48.6              | 0.21         |
| 12          | 38.8              | 0.3          |
| 16          | 25.3              | 0.43         |
| 20          | 17                | 0.52         |
| 24          | 15.6              | 0.54         |
| 28          | 14.8              | 0.57         |
| 32          | 14.3              | 0.58         |
| 36          | 13.9              | 0.59         |
| 40          | 13.9              | 0.59         |

The medium in which MNPs are dispersed also can affect the heating efficacy of MNPs. Based on Equations (3)–(7), Rosensweig’s calculations demonstrated a dependence of the heating rate $\Delta T/\Delta t$ on the medium viscosity at 3 different frequencies [20]. We performed systematic calculations of $\text{SLP}_{\text{max}}$ in the viscosity range from 1 mPa·s to 10 mPa·s for MNPs with various K. The results of the relative $\text{SLP}_{\text{max}}(\eta)/\text{SLP}_{\text{max}}(\eta = 1 \text{ mPa·s})$ for the fluid of FO MNPs are presented in Figure 5. As can be seen in Figure 5, for FO MNPs with the value of K in NB-region (9 kJ/m$^3$), $\text{SLP}_{\text{max}}$ decreases very little with increasing $\eta$. In contrast, there is a large decrease in the $\text{SLP}_{\text{max}}$ when the value of $\eta$ is going from 1 kJ/m$^3$ to 4 mPa·s for 20 kJ/m$^3$, and 41 kJ/m$^3$ FO MNPs. It is noted that the value of critical anisotropy at 4 mPa·s for the field frequency of 100 kHz is 60 kJ/m$^3$ (Table 2). Therefore, the decrease of $\text{SLP}_{\text{max}}$ with increasing $\eta$ might occur when the value of anisotropy is smaller than $K_c$. In other words, this behavior happens when the K of FO MNPs is in the B-region. These calculations indicated that the FO MNPs with the K in the N- or NB-regions are much better for MIH applications in highly viscous conditions. The observation of weak and strong decrease of the heating power with increasing viscosity, will be discussed as compared with experimental results in the following section.

### 3.4. A Comparison with Experimental Results

To compare the results from the experiments with the theoretical ones in a simple way, we have investigated SLP of the same MNPs but varying viscosity. Previously we reported the SAR measurements carried out at the field of 178 kHz and 5.18 kA/m (65 Oe) for bare CFO and MFO MNPs suspended in water fluid with added agar forming media with viscosity up to about 2 mPa·s, and observed strong and weak decrease of SAR with an increase of $\eta$, respectively for CFO and MFO, which is in agreement with the LRT prediction [40]. For comparing the results from the experiments with the theoretical ones, we studied two ferrofluids of 20 nm low-K MnFe$_2$O$_4$ and 15 nm high-K CoFe$_2$O$_4$ MNPs.
coated with chitosan. They were prepared by co-precipitation. To create the magnetic fluids with different viscosity, the MNPs suspension was mixed with various agar concentrations. The value of viscosity extended up to about 8 mPa·s by adding more agar amounts. The fabrication of samples with various viscosities as well as the method of viscosity measurement were described earlier [40] as were the experimental details of the synthesis and the coating procedure by chitosan [41]. As discussed in our previous reports, chitosan has been widely used in biomedicine due to its biocompatibility and biodegradability [41]. Based on the measured magnetization curves shown in Figure S3, the thickness of chitosan coating layer was estimated to be around 4 nm. The value of Ms, Hc and Keff for MFO and CFO NPs (shown details in Supplementary Section S3) are presented in Table 4.

Table 4. Values of Keff at different frequencies for fluids with various viscosities (η (mPa·s)).

| Sample            | Ms (emu/g) | Hc (Oe) | Keff (kJ/m³) |
|-------------------|------------|---------|--------------|
| MFO (uncoated)    | 60.9       | 72      | -            |
| MFO (coated)      | 51.9       | 72      | 11           |
| CFO (uncoated)    | 67.2       | 875     | -            |
| CFO (coated)      | 57.4       | 875     | 62           |

In addition to the field of 178 kHz, 5.18 kA/m (provided by a commercial generator RDO HFI 5 kW [40]), the calorimetric measurements were additionally conducted at two fields of the same amplitude of 15.9 kA/m (200 Oe) with frequencies of 340 kHz and 450 kHz (provided by a commercial generator UHF-20A [42]), to seek evidence of SAR behavior changing with increasing field frequency. The temperature elevation with time, T(t), was monitored by using the same commercial optical sensor (GaAs-Opsens) for both MIH sets up.

The heating curves, measured at the lower field, for the two series of MFO and CFO samples in solutions of various agar concentrations are presented in Figure 6. The values of SARexp were calculated from the fitting of the temperature rising curves T(t) for the whole time range following the method described in reference [40].
Figure 6. Hyperthermia curves measured at field frequency $f = 178$ kHz, $H = 5.18$ kA/m for (a) MFO and (b) CFO ferrofluids of various viscosities.

In order to compare the experimental and theoretical SAR, we calculated the Néel-Brownian relaxation experimental SAR$_{\text{exp}}^{\text{LRT}}$ by using the Equation:

$$\text{SAR}_{\text{exp}}^{\text{LRT}} = \text{SAR}_{\text{exp}} - \text{SAR}_{\text{exp}}^{\text{hys}},$$

where SAR$_{\text{exp}}$ is the SAR contribution by hysteresis mechanism, whose estimation is described in Supplementary Section S3, similarly to the approach reported in [42]. The results of calculated SAR$_{\text{exp}}^{\text{LRT}}$ obtained from the measurements at 340 kHz and 450 kHz. They are gathered in Supplementary Section S4. As can be seen, for the MFO samples with $K = 11$ kJ/m$^3$ and $H_c$ were close to or smaller than the AFM amplitudes, the contribution of SAR$_{\text{exp}}^{\text{hys}}$ is less than 2.5% of the whole heating power. However, for the CFO samples with $K = 62$ kJ/m$^3$ and $H_c$ much larger than the field amplitude used, the maximum SAR$_{\text{exp}}^{\text{hys}}$ contributions were 17%, 16% and 9% for 178, 340 and 145 kHz, respectively.

In order to discuss about the impact of AFM frequency on the SAR characteristics relevant to the relaxation mechanisms, we calculated the ratio of SAR($\eta$)/SAR($\eta = 1$ mPa·s) for all the MFO and CFO samples of various viscosities measured at the 3 frequencies (see also Tables S1–S3), the dependences of which are shown in Figure 7.

Figure 7. Relative SAR$_{\text{exp}}$ and SAR$_{\text{exp}}^{\text{LRT}}$ measured at field of (a) 5.18 kA/m, 178 kHz; (b) 15.9 kA/m, 340 kHz; and (c) 15.9 kA/m, 450 kHz.

Firstly, it can be noted that the decrease of SAR with increasing viscosity is experimentally observed in all the cases, so that the impact of the hysteresis contribution is insignificant.
Secondly, Figure 7a,b suggest that the strong and weak decrease of SAR with increasing viscosity, depicted respectively for CFO and MFO, confirm our previous experiment reported for $\eta \leq 2.12$ mPa·s [40] and the agreement with the LRT theory prediction shown in Figure 5. While such a behavior is natural for the case of the field (178 kHz, 65 Oe) with the parameter $\xi$ of about 0.7, it is worth noting that such behavior ‘survived’ to the field of 340 kHz and 15.9 kA/m with $\xi$, of about 2. The trend of decreasing SAR with increasing viscosity $\eta$ in our experiments is also in agreement with the observation for $\gamma$-Fe$_2$O$_3$ ($D = 7.1$ nm, $\sigma = 0.37$) and CoFe$_2$O$_4$ ($D = 9.7$ nm, $\sigma = 0.35$) MNPs where SAR decreased, respectively, about 20% and 80% when the viscosity increased from 0.75 to 335 mPa·s [22]. In fact, it was found that SLP value from MNPs dispersed in water is higher than in glycerol for the same type of MNPs, MNP dose, and AMF condition [43]. A similar phenomenon was observed in the cellular environment as well, in which the measured SLP value decreased by half associated with attenuation of the Brownian relaxation in cellular conditions [44]. Thirdly, while the MFO ferrofluids remain almost not impacted by the field frequency used, it is interesting to observe for CFO samples a clear shift from high K toward low-K characteristic behavior when the used field frequency increases from 178 kHz to 450 kHz. In particular, Figure 7c for the case of $f = 450$ kHz indicates that the relative SAR versus $\eta$ for the CFO MNPs approaches to the type of very weak decrease of the heating power with increasing the media viscosities, similarly to that of MFO MNPs. This observation is in good agreement with the scheme shown in Figure S7, according to which the MFO MNPs of $K = 11$ kJ/m$^3$ are predicted to exhibit the SAR contributed mainly from the Neel or overlapped Neel-Brownian relaxation losses depending not on the used field frequency, and the dissipation mechanism contributing to the SAR for the CFO MNPs with $K = 62$ kJ/m$^3$ belongs to the pure Brownian region for AMF with $f$ below about 460 kHz and changes to the Neel-Brown or Neel type above this frequency.

4. Conclusions

In summary, in addition to the peak position $D_c$ and its amplitude SLP$_{max}$, we have introduced a peak width $\Delta D_c$ and performed systematic analyses of the three parameters against the magnetic anisotropy of MNPs, fluid viscosities and the frequency of the alternating magnetic field. High K MNPs have been shown to exhibit domination of Brownian loss while it becomes that of Néel loss in low K ones. To the best of our knowledge, our results have demonstrated for the first time the transition from Néel to Brownian loss region not to occur in a continuous way, but at critical anisotropy $K_c$ which increases with the frequency of the alternating magnetic field and the viscosity of the ferrofluid. We have pointed out that, for a given material, fabrication of MNPs with higher anisotropy up to $K_c$ can improve the heating power as much as 35% thanks to the offsetting of the polydispersity-caused reduction. From the calculation and experimental results, it appears that low K MNPs are in general better for MIH applications in highly viscous conditions than those of high K ones.

Supplementary Materials: The following are available online at https://www.mdpi.com/article/10.3390/ma14081875/s1, Figure S1: (a) $D_c$ versus $K$ for various AMF frequencies. (b) The width $\Delta D_c$, and $D_c$ versus $K$ at $f = 500$ kHz showing 3 characteristic N, NB and B regions; Figure S2: Polydispersity-caused SLP reduction calculated at $f = 100$ kHz for iso-dispersion $\sigma = 0.2$ FO MNPs as a function of anisotropy $K$, Figure S3: Magnetization curves measured for as-synthesized and chitosan coated (a) MFO, and (b) CFO MNPs; Figure S4: The initial magnetization curves of MFO and CFO MNPs. The solid lines represent the fitting curve assuming “the law of approach to saturation”; Figure S5: Hyperthermia curves measured at fields of frequency $f = 340$ kHz, $H = 15.9$ kA/m (200 Oe) for (a) MFO and (b) CFO ferrofluids of various viscosities; Figure S6: Hyperthermia curves measured at fields of frequency $f = 450$ kHz, $H = 15.9$ kA/m for (a) MFO and (b) CFO ferrofluids of various viscosities; Figure S7: Illustration scheme for the MIH experiments for CFO and MFO MNPs, Table S1: Values of SAR$_{exp}$, SAR$_{exp}^{hys}$, SAR$_{LRT}^{exp}$, and $\frac{SAR_{LRT}^{exp}}{SAR_{exp}^{hys}}$ at $5.18$ kA/m, 178 kHz; Table S2: Values
of $\text{SAR}_{\text{phys}}$, $\text{SAR}_{\text{exp}}$, $\text{SAR}_{\text{LRT}}$, and $\text{SLP}_{\text{LRT}}$ at 15.9 kA/m, 340 kHz; Table S3: Values of $\text{SAR}_{\text{exp}}$, $\text{SAR}_{\text{phys}}$, $\text{SAR}_{\text{LRT}}$, and $\text{SLP}_{\text{LRT}}$ at 15.9 kA/m, 450 kHz.

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**References**

1. Pankhurst, Q.A.; Thanh, N.T.K.; Jones, S.K.; Dobson, J. Progress in Applications of Magnetic Nanoparticles in Biomedicine. *J. Phys. D* 2009, 42, 224001. [CrossRef]

2. Kumar, C.S.S.R.; Mohammad, F. Magnetic nanomaterials for hyperthermia-based therapy and controlled drug delivery. *Adv. Drug Deliv. Rev.* 2011, 63, 789–808. [CrossRef]

3. Gupta, A.K.; Gupta, M. Synthesis and surface engineering of iron oxide nanoparticles for biomedical applications. *Biomaterials* 2005, 26, 3995–4021. [CrossRef] [PubMed]

4. Hergt, R.; Dutz, S.; Muller, R.; Zeisberger, M. Magnetic particle hyperthermia: Nanoparticle magnetism and materials development for cancer therapy. *J. Phys. Condens. Matter* 2006, 18, S2919–S2934. [CrossRef]

5. Thuy, T.T.; Maenosono, S.; Thanh, N.T.K. Next Generation Magnetic Nanoparticles for Biomedical Applications. In *Magnetic Nanoparticles: From Fabrication to Clinical Applications*, 1st ed.; Thanh, N.T.K., Ed.; CRC Press: New York, NY, USA, 2012; pp. 99–128.

6. Gavilán, H.; Brollo, M.E.F.; Gutiérrez, L.; Veintemillas-Verdaguer, S.; Morales, M.D.P. Controlling the Size and Shape of Uniform Magnetic Iron Oxide Nanoparticles for Biomedical Applications. In *Clinical Applications of Magnetic*, 1st ed.; Thanh, N.T.K., Ed.; CRC Press: New York, NY, USA, 2018; pp. 3–24.

7. Obaidat, I.M.; Issa, B.; Haik, Y. Magnetic properties of magnetic nanoparticles for efficient hyperthermia. *Nanomaterials* 2015, 5, 63–89. [CrossRef]

8. Hilger, I. In vivo applications of magnetic nanoparticle hyperthermia. *Int. J. Hyperth.* 2013, 29, 828–834. [CrossRef] [PubMed]

9. Jeun, M.; Kim, Y.J.; Park, K.H.; Paek, S.H.; Bae, S. Physical Contribution of Néel and Brown Relaxation to Interpreting Intracellular Hyperthermia Characteristics Using Superparamagnetic Nanofluids. *J. Nanosci. Nanotechnol.* 2013, 13, 5719–5725. [CrossRef]

10. Lin, M.; Huang, J.; Sha, M. Recent Advances in Nanosized Mn-Zn Ferrite Magnetic Fluid Hyperthermia for Cancer Treatment. *J. Nanosci. Nanotechnol.* 2014, 14, 792–802. [CrossRef] [PubMed]

11. Hedayatnasab, Z.; Abnisa, F.; Daud, W.M.A.W. Review on magnetic nanoparticles for magnetic nanofluid hyperthermia application. *Mater. Des.* 2017, 123, 174–196. [CrossRef]

12. Derfus, A.M.; Maltzahn, G.V.; Harris, T.J.; Duza, T.; Vecchio, K.S.; Ruoslahti, E.; Bhatia, S.N. Remotely triggered release from magnetic nanoparticles. *Adv. Mater.* 2007, 19, 3932–3936. [CrossRef]

13. Brazel, S.C. Magnetothermally-responsive nanomaterials: Combining magnetic nanostructures and thermally-sensitive polymers for triggered drug release. *Pharm. Res.* 2009, 26, 644–656. [CrossRef]

14. Stanley, S.A.; Gagner, J.E.; Damanpour, S.; Yoshida, M.; Dordick, J.S.; Friedman, J.M. Radio-Wave Heating of Iron Oxide Nanoparticles Can Regulate Plasma Glucose in Mice. *Science* 2012, 336, 604–608. [CrossRef]

15. Etheridge, M.L.; Xu, Y.; Rott, L.; Choi, J.; Glasmer, B.; John, C.; Bischof, R.F. Heating of magnetic nanoparticles improves the thawing of cryopreserved biomaterials. *Technology* 2014, 2, 229–242. [CrossRef]

16. Manuchehrabadi, N.; Gao, Z.; Zhang, J.; Ring, H.L.; Shao, Q.; Liu, F.; McDermott, M.; Fok, A.; Rabin, Y.; Brockbank, K.G.M.; et al. Improved Tissue Cryopreservation using Inductive Heating of Magnetic Nanoparticles. *Sci. Transl. Med.* 2017, 9, eaah4586. [CrossRef]

17. Manuchehrabadi, N.; Shi, M.; Roy, P.; Han, Z.; Qiu, J.; Xu, F.; Lu, T.J.; Bischof, J. Ultrarapid Inductive Rewarming of Vitrified Biomaterials with Thin Metal Forms. *Ann. Biomed. Eng.* 2018, 46, 1857–1869. [CrossRef]
18. Pham, H.N.; Pham, T.H.G.; Nguyen, D.T.; Phan, Q.T.; Le, T.T.H.; Ha, P.T.; Do, H.M.; Hoang, T.M.D.; Nguyen, X.P. Magnetic inductive heating of organs of mouse models treated by copolymer coated Fe₂O₃ nanoparticles, Adv. Nat. Sci. Nanosci. Nanotechnol. 2017, 8, 025013. [CrossRef]

19. Carrey, J.; Mehdaoui, B.; Respaud, M. Simple models for dynamic hysteresis loops calculation: Application to hyperthermia optimization. J. Appl. Phys. 2011, 109, 083921. [CrossRef]

20. Rosensweig, R.E. Heating magnetic fluid with alternating magnetic field. J. Magn. Magn. Mater. 2002, 252, 370–374. [CrossRef]

21. Maenosono, S.; Saita, S. Theoretical Assessment of FePt Nanoparticles as Heating Elements for Magnetic Hyperthermia. IEEE Trans. Magn. 2006, 42, 1638–1642. [CrossRef]

22. Fortin, J.P.; Wilhelm, C.; Servais, J.; Menager, C.; Bacri, J.C.; Gazeau, F. Size-Sorted Anionic Iron Oxide Nanoparticles as Colloidal Mediators for Magnetic Hyperthermia. J. Am. Chem. Soc. 2007, 129, 2628–2635. [CrossRef] [PubMed]

23. Habib, A.H.; Ondeck, C.L.; Chaudhary, P.; Bockstaller, M.R.; McHenry, M.E. Evaluation of Iron-cobalt/ferrite core-shell nanoparticles for cancer thermotherapy. J. Appl. Phys. 2008, 103, 07A307. [CrossRef]

24. Phong, P.T.; Nguyen, L.H.; Manh, D.H.; Lee, I.J.; Phuc, N.X. Computer simulations of contributions of Néel and Brown relaxation to Specific Loss Power of magnetic fluids in Hyperthermia. J. Electron. Mater. 2017, 46, 2393–2405. [CrossRef]

25. Deatsch, A.E.; Evans, B.A. Heating efficiency in magnetic nano particle hyperthermia. J. Magn. Magn. Mater. 2014, 354, 163–172. [CrossRef]

26. Suto, M.; Hirota, Y.; Mamiya, H.; Fujita, A.; Kasuya, R.; Tohji, K.; Jeyadevan, B. Heat dissipation mechanism of magnetite nanoparticles in magnetic fluid hyperthermia. J. Magn. Magn. Mater. 2009, 321, 1493–1496. [CrossRef]

27. Gonzales-Weimueller, M.; Zeisberge, M.; Krishnan, K.M. Size-dependent heating rates of iron oxide nanoparticles for magnetic fluid hyperthermia. J. Magn. Magn. Mater. 2009, 321, 1947–1950. [CrossRef]

28. Krishnan, K.M. Biomedical nanomagnetics: A spin through possibilities in imaging, diagnostics, and therapy. IEEE Trans. Mag. 2010, 46, 2523–2558. [CrossRef]

29. Khandhar, A.P.; Ferguson, R.M.; Simon, J.A.; Kriifhnan, K.M. Tailored magnetic nanoparticles for optimizingmagnetic fluid hyperthermia. J. Biomed. Mater. Res. Part A 2012, 100A, 728–737. [CrossRef]

30. Larrique, L.; Innocenti, C.; Kalaiavani, T.; Awwad, A.; Sanchez-Duque, M.; Guari, Y.; Larionova, J.; Guerin, C.; Montero, J.L.; Barragan-Montero, V.; et al. Water-dispersible sugar-coated iron oxide nanoparticles: An evaluation of their relaxometric and magnetic hyperthermia properties. J. Am. Chem. Soc. 2011, 133, 10459–10472. [CrossRef]

31. Guardia, P.; Corato, R.D.; Larrique, L.; Wilheim, C.; Espinosa, A.; Garcia-Hernandez, M.; Gazeau, F.; Manna, L.; Pellegrino, T. Water-soluble Iron Oxide Nanocubes with High Values of Specific Absorption Rate for Cancer Cell Hyperthermia Treatments. ACS Nano 2012, 6, 3080–3091. [CrossRef]

32. Vreeland, E.C.; Watt, J.; Schober, G.B.; Hance, B.G.; Austin, M.J.; Monson, T.C.; Hudak, N.S.; Maldonado-Camargo, L.; et al. Enhanced nanoparticles size control by extending Lamer’s Mechanism. Chem. Mater. 2015, 27, 6059–6066. [CrossRef]

33. Khurshid, H.; Alonso, J.; Nemati, Z.; Phan, M.H.; Mukherjee, P.; Fdez-Gubieda, M.L.; Barandiaran, J.M.; Srikanth, H. Anisotropy effects in magnetic hyperthermia: A comparison between spherical and cubic exchange-coupled FeO/Fe₂O₃ nanoparticles. J. Appl. Phys. 2015, 117, 17A337. [CrossRef]

34. Gonzalez-Fernandez, M.A.; Torres, T.E.; Andres-Verges, M.; Castro, R.; dela Presa, P.; Serna, C.J.; Morales, M.P.; Marquina, C.; Ibarra, M.R.; Goya, G.F. Magnetic nanoparticles for power absorption: Optimizing size, shape and magnetic properties. J. Solid State Chem. 2009, 182, 2779. [CrossRef]

35. Pilien, M.P.; Moumen, N.; Hochepied, J.H.; Bonville, P.; Veiller, P. Control of the size of cobalt ferrite nanoparticles: Synthesis and properties. J. Phys. Fr. 1997, 7, C1-505–C1-508. [CrossRef]

36. Lahiri, B.B.; Ranoo, S.; Muthukumaran, T.; Philip, J. Magnetic hyperthermia in water based ferrofluids: Effects of initial susceptibility and size polydispersity on heating efficiency. AIP Conf. Proc. 2018, 1942, 040019.

37. Levy, M.; Quarta, A.; Figurerola, A.; Wilhelme, C.; Garcia-Hermandez, M.; Genovese, A.; Faluhi, A.; Alloysseau, D.; Buonansi, R.; Cozzoli, P.D.; et al. Correlating magneto-structural properties to hyperthermia performance of highly monodisperse iron oxides nanoparticles prepared by a seeded-growth route. Chem. Mater. 2011, 23, 4170–4180. [CrossRef]

38. Lee, J.H.; Jang, J.T.; Choi, J.S.; Moon, S.H.; Noh, S.H.; Kim, J.W.; Kim, J.G.; Kim, I.S.; Park, K.I.; Cheon, J.W. Exchange-coupled Magnetic Nanoparticles for Efficient Heat Induction. Nanotechnology 2011, 6, 418–422. [CrossRef] [PubMed]

39. Martinez-Baubeta, C.; Simeonidis, K.; Makridis, A.; Angelakaris, M.; Iglesias, O.; Guarida, P.; Cabot, A.; Yeada, L.; Estrade, S.; Peiro, F.; et al. Learning from Nature to Improve the Heat Generation of Iron-Oxide Nanoparticles for Magnetic Hyperthermia Applications. Sci. Rep. 2013, 3, 1652–1659. [CrossRef]

40. Phong, P.T.; Nguyen, L.H.; Phong, L.T.H.; Nam, P.H.; Manh, D.H.; Lee, I.J.; Phuc, N.X. Study of specific loss power of magnetic fluids with various viscosities. J. Magn. Magn. Mater. 2017, 428, 36–42. [CrossRef]

41. Mai, T.T.; Ha, P.T.; Pham, H.N.; Le, T.T.H.; Pham, H.L.; Pham, T.B.H.; Tran, D.L.; Nguyen, X.P. Chitosan and O-carboxymethyl chitosan modified Fe₂O₃ for hyperthermic treatment. Adv. Nat. Sci. Nanosci. Nanotechnol. 2012, 3, 015006. [CrossRef]

42. Nguyen, L.H.; Oanh, V.T.K.; Nam, P.H.; Doan, D.H.; Truong, N.X.; Ca, N.X.; Phong, P.T.; Hong, L.V.; Lam, T.D. Increase of magnetic hyperthermia efficiency due to optimal size of particles: Theoretical and experimental results. J. Nanopart. Res. 2020, 258, 1–16. [CrossRef]
43. Kalambur, V.S.; Han, B.; Hammer, B.E.; Shield, T.W.; Bischof, J.C. In vitro characterization of movement, heating and visualization of magnetic nanoparticles for biomedical applications. *Nanotechnology* **2005**, *16*, 1221. [CrossRef]

44. Di Corato, R.; Espinosa, A.; Lartigue, L.; Tharaud, M.; Chat, S.; Pellegrino, T.; Menager, C.; Gazeau, F.; Wilhelm, C. Magnetic hyperthermia efficiency in the cellular environment for different nanoparticle designs. *Biomaterials* **2014**, *35*, 6400–6411. [CrossRef] [PubMed]