Recent advances and future prospects of iron oxide nanoparticles in biomedicine and diagnostics

N. V. Srikanth Vallabani1 · Sanjay Singh1

Received: 31 March 2018 / Accepted: 7 May 2018
© The Author(s) 2018

Abstract
Superparamagnetic iron oxide nanoparticles (SPIONs) are considered as chemically inert materials and, therefore, being extensively applied in the areas of imaging, targeting, drug delivery and biosensors. Their unique properties such as low toxicity, biocompatibility, potent magnetic and catalytic behavior and superior role in multifunctional modalities have epitomized them as an appropriate candidate for biomedical applications. Recent developments in the area of materials science have enabled the facile synthesis of iron oxide nanoparticles (IONPs) offering easy tuning of surface properties and surface functionalization with desired biomolecules. Such developments have enabled IONPs to be easily accommodated in nanocomposite platform or devices. Additionally, the tag of biocompatible material has realized their potential in myriad applications of nanomedicines including imaging modalities, sensing, and therapeutics. Further, IONPs enzyme mimetic activity pronounced their role as nanozymes in detecting biomolecules like glucose, and cholesterol etc. Hence, based on their versatile applications in biomedicine, the present review article focusses on the current trends, developments and future prospects of IONPs in MRI, hyperthermia, photothermal therapy, biomolecules detection, chemotherapy, antimicrobial activity and also their role as the multifunctional agent in diagnosis and nanomedicines.

Keywords Magnetic resonance imaging · Feraheme · Theranostics · Computed tomography · Cell labeling · Nanozymes · Magnetic separation

Introduction
IONPs possess unique properties, which are used to display several applications in biomedicine such as diagnostics, imaging, hyperthermia, magnetic separation, cell proliferation, tissue repair and drug delivery. Although nanostructures of iron, cobalt, and nickel are known to exhibit superparamagnetic properties and high magnetic susceptibility, IONPs such as magnetite (Fe3O4), hematite (α-Fe2O3) and maghemite (γ-Fe2O3), are the most studied magnetic nanoparticle type. Owing to this property, IONPs display aggregation behavior under the magnetic field, which can be suspended again as a stable suspension after removal of the external magnetic field. In addition, the better colloidal stability, biocompatibility, and persistence magnetic properties of IONPs make them an excellent candidate for biomedical applications (Huang et al. 2009; Isa Karimzadeh 2017).

Fe3O4 NPs differ from other IONPs due to the presence of both Fe2+ and Fe3+ combinations, where divalent ions are organized at the octahedral sites and trivalent ions are split across the tetrahedral and octahedral sites. However, α-Fe2O3 contains Fe3+ ions distributed at their octahedral sites and in case of γ-Fe2O3 (termed oxidized magnetite), Fe3+ cations are distributed in octahedral and tetrahedral sites along with Fe2+ cation vacancies located at octahedral sites (Wu et al. 2015b). Due to their feasible polymorphism and their electron hopping nature, these IONPs were classified as potential candidates in both biological and technical applications. In recent years, to enhance the use of IONPs in advanced applications/technologies NPs are altered by the creation of active layers supported by polymers, inorganic metal/metal oxides or bioactive molecules (Gupta and Gupta 2005). The surface engineering of IONPs can be achieved by several methods through layering a coating material over the iron oxide core, to form core–shell structure or the NPs are dispersed in a matrix to form the beads (Gupta et al. 2007).
In addition, a Janus structure can be formed with one-half of IONPs and the rest with functional material, further, IONPs are embedded between two functional materials to form a shell–core–shell structure (Wu et al. 2015b).

Several methods like thermal decomposition, co-precipitation, sol–gel, microemulsion, hydro-thermal, sono-chemical, microwave, electrochemical and biosynthesis were evolved to synthesize IONPs (Huber 2005; Wu et al. 2015b). However, the relation between size, shape, and magnetism in IONPs plays a crucial role in exhibiting their properties. For instance, Fe₂O₃ and Fe₃O₄ NPs display different ferromagnetism at room temperature. Further, IONPs tend to lose their dispersity after long-term due to aggregation of particles and their magnetism gets diminished due to oxidation in air. Thus different approaches are implemented to stabilize the NPs in an inert atmosphere and also to make them water-soluble at physiological pH, for applications in nanomedicine (Wu et al. 2015b).

For biomedical applications and in vivo studies, low toxicity, biocompatibility, biodegradability, long retention time, and magnetism to localize the IONPs at the target play a crucial role (Wu et al. 2015b). In diagnosis IONPs, acts as a probe in magnetic resonance imaging (MRI), Positron emission tomography (PET), near-infrared fluorescence (NIRF) imaging (Ju et al. 2017; Xie et al. 2010) and in biosensors for detection of biomolecules like glucose, proteins, urea, and uric acid (Chen et al. 2012; Wu et al. 2015a; Yu et al. 2009). Comparatively, IONPs gained attention in therapeutic nanomedicine ranging from cancer treatment to antimicrobial activity (Nehra et al. 2018; Patra et al. 2017). In theranostics, IONPs are applied as nano-carriers, for enhancing the drug activity in combination therapy (IONPs and chemotherapeutic drugs) or as hyperthermia agents (Ren et al. 2012). Therefore, in the present review article, we focused on the IONPs applications in the domains of diagnosis and therapeutics.

**IONPs as imaging probe**

**Role of iron oxide nanoparticles as contrast agent in Magnetic Resonance Imaging**

MRI utilizes gradients of magnetic fields, radio waves and electric fields to elucidate the detailed internal structures of the body. MRI has a wide range of applications in detecting diseases or disorders of brain, heart, liver, blood vessels, and other vital organs. Recent research advancements have produced several excellent magnetic contrast agents such as gadolinium, superparamagnetic iron oxides, ultrasound (5–10 nm) superparamagnetic iron oxides, gadolinium doped carbon nanotubes, quantum dots embedded paramagnetic micelles and soft nanoparticles such as liposomes, perfluorocarbon emulsions, etc. (Emily and Waters 2008; Liu et al. 2017). Further, IONPs are prepared in combination with other NPs, proteins or dyes to achieve multiple applications in a single stage, for instance, MRI and immunohistochemical staining of cancer cells was executed using ferrimagnetic H-ferritin (M-HFn) nanoparticles, dual MRI and CT imaging of tumor was simultaneously fulfilled by assembling gold (Au) nanocages, Fe₃O₄ NPs and triple functional iron oxide nanoparticles (Fig. 1) with Cy5.5 dye and ⁶⁴Cu-DOTA chelate were developed for MRI, positron emission tomography (PET) and near-infrared fluorescence (NIRF) imaging (Cai et al. 2015; Wang et al. 2016; Xie et al. 2010).

Ferumoxytol (Feraheme) is one of the types of magnetic IONPs approved by the US Food and Drug Administration (FDA) for the treatment of patients suffering from iron deficiency with chronic kidney disease (CKD). It consists of a non-stoichiometric magnetite nanoparticle capped by poly glucose sorbitol carboxymethyl ether. Recently many imaging and therapeutic applications have been performed using ferumoxytol and the results suggest that it can be used in MR imaging with IONP cell labels for in vivo tracking of stem cells and also can be applied for non-invasive monitoring of stem cell therapies in pre-clinical and clinical setting (Castaneda et al. 2011). Moreover, studies delineated

**Fig.1** Schematic illustration of the multifunctional HSA-IONPs for triple active MRI/PET/NIRF imaging. The pyrolysis-derived IONPs were incubated with dopamine, after which the particles became moderately hydrophilic and could be doped into HSA matrices in a way similar to drug loading. Reprinted with permission from ref (Xie et al. 2010) Copyright (2010) Elsevier
ferumoxytol-enhanced MRI was more sensitive for detection of early necrosis in tumor cells compared to other contrast agents (Aghighi et al. 2015). Reports also revealed that ferumoxytol gained interest to be used in renal failure patients as an alternative to gadolinium-based contrast agents for vascular MRI (Hope et al. 2015). Furthermore, as the feraheme is taken up by macrophages in liver, lymph nodes and spleen they can be explored for imaging macrophages, tumors, vascular lesions and other organs (Bashir et al. 2015; Vasanawala et al. 2016).

IONPs are a versatile class of material, which can be tuned to exhibit multifunctional applications. In one such attempt, Xie et al. (Xie et al. 2010) have developed dopamine modified IONPs, which was then encapsulated into human serum albumin (HSA) matrices. It was also shown that the HSA coated IONPs can also be labeled with two different dyes, $^{64}$Cu-DOTA and Cy5.5, to impart multiplexed imaging capability and tested them in a subcutaneous U87MG xenograft mouse model. Results revealed that a tri-modality imaging (including MRI, PET, and NIRF) was very much possible under ex vivo and in vivo experimental condition. HSA coating manifested longer blood circulation time, high extravasation and accumulation in targeted tissues and low uptake in macrophages in the nearby area of tumor.

In the current context, image-guided photothermal therapy (PTT) is being looked as a promising alternative therapeutic modality to the most of the conventional methods. PTT is also expected to have potential to offer a better precision therapy alternative. Owing to the recent developments in material science, it is possible to synthesize the materials of our interest with variable size, shape, and composition. However, producing multicomponent materials with desired dimensions and stability still remains a challenge. Considering this, Ju et al. have developed a monodispersed composite material (Au–Fe$_2$C Janus NPs) and used them as multifunctional cancer theranostics. These 12 nm particles exhibited a broad absorbance pattern under near infrared region, which lead to the generation of significant photothermal effect when irradiated with 808 nm laser light. This nanocomposite offered excellent optical and magnetic properties, which was found to be a promising method for triple-modal MRI/multispectral photoacoustic tomography (MSOT)/CT imaging both in in vitro and in vivo experimental models. Authors also modified this magnetic nanocomposite with HER2 affibody, which showed higher accumulation and deep tissue penetration in tumors than unconjugated particles (Ju et al. 2017). In another study by Monaco et al. developed a multi-layered nano-system composed of Fe$_3$O$_4$ NPs, coated with inner silica and outer Au layers. These NPs were entrapped into polymeric micelles and surface was conjugated with folic acid to offer them water solubility and target recognition. This novel nano-system was shown applications in targeting and magnetic resonance–photoacoustic based dual imaging modality. The significance of the complex system lies in having optical properties of gold NPs and a high dielectric constant of silica NPs ensuring strong light absorption capability (Fig. 2). Hence, they were utilized as a bimodal MRI-photoacoustic imaging (PAI) agent for imaging and detection of ovarian cancer (Monaco et al. 2017).

Malignant cells are characterized to have a significantly high rate of metabolism and glucose uptake. Utilizing this mechanism, cancer tissues are visualized under PET, involving high uptake of a radiolabelled glucose analog, $[^{18}$F$]$-2-fluoro-2-deoxy-D-glucose (Lindholm et al. 1993). It is reported that the glucose transporter (Glut) proteins are found in the plasma membrane of mammalian cells, which facilitates the transport of glucose in the cytoplasm. Although there are several Glut proteins, however, Glut-1 has been shown to be involved in the high transportation of glucose in cancer cells (Singh 2017). Therefore, Glut proteins are considered as one of the suitable markers to selectively identify the cancer cells/tissues. The conjugation of Glut antibody with IONPs was shown to diagnose hemangioma (a condition in which noncancerous growths of blood vessels occur) through their MRI contrast imaging modality. The study was focussed on the differentiation of infantile hemangioma from vascular malformation, as Glut-1 is only expressed in cells of infant hemangioma (Sohn et al. 2015).

In general, IONPs acts as a probe for negative contrast (T$_2$ contrast agents) due to their superparamagnetic behaviour and large magnetic moment. However, a typical dark signal produced in the T$_2$ image can cause difficulty in distinguishing the areas of interest with calcium deposits, bleeding and glioma imaging. To overcome the limitation, Juan et al. synthesized citrate coated IONPs (C-ESION) with excellent positive (T$_1$ imaging) and negative contrast
through modulating the composition and coating thickness. In addition, authors demonstrated that the coating chemistry on NPs surface can change their relaxometric properties, which can be manipulated to generate particles with different contrasts. Results explained C-ESION120 displayed $T_1$ weighed contrast and C-ESION140 showed $T_2$ contrast signal characteristics. Hence, the modified coating enabled the maghemite NPs for $T_1$ high-resolution MR angiography and also provided standard $T_2$ contrast to utilizing them for a full range of applications in MRI (Pellico et al. 2017). Further, Ning et al. synthesized Gd-doped and PEG-coated IONPs (PEG-GdIO) having $T_1-T_2$ bimodal contrast ability and demonstrated the simultaneous $T_1-T_2$ contrast imaging in mice bearing glioma. Results revealed that after 1 h of NPs injection $T_1$ and $T_2$ weighted images showed brighter and darker contrast compared to pre-injection MR images. Moreover, the contrast enhancement was analyzed by contrast to noise ratio and significant improvement in signals was found for both $T_1$ and $T_2$ contrast images. Hence, it was concluded that PEG-GdIO NPs can be used as dual contrast agent for brain glioma detection (Xiao et al. 2014). Cha et al. modified $\text{Fe}_3\text{O}_4$ NPs ($\text{Fe}_3\text{O}_4$@GCP—$\text{Fe}_3\text{O}_4$ surface modified with glutathione, cyclodextrin and polymer) through polymer coating composed of $\beta$-cyclodextrin core and poly [2-(dimethylamino) ethyl methacrylate] arms and in association with reduced glutathione (GSH) as a model drug. The designed platform was expected for simultaneous diagnosis and treatment purposes. Authors suggested $\text{Fe}_3\text{O}_4$ NPs coated with these star polymers exhibited more GSH association compared to linear polymers and showed better stability in serum solutions. Further $\text{Fe}_3\text{O}_4$@GCP rendered low cytotoxicity and possessed enhanced $T_1$ MRI characteristics. Results showed significant bright enhancement observed for $T_1$ weighted images of liver visualization suggesting that the modified NPs can be used for diagnosis and treatment of chronic liver diseases (Cha et al. 2017).

**Use of iron oxide nanoparticles as contrast agent in computed tomography**

CT is an X-ray based whole body imaging technique that combines series of computer processed X-ray images to construct the cross-sectional images of specific areas. CT is used to diagnose diseases or internal injuries in blood vessels, bones, soft tissues and other parts of the body. Clinically approved CT contrast agents for intravenous injection are iodinated small molecules or barium suspensions. Due to hypersensitive to iodinated contrast and renal impaired patients there is a need for better contrast agents. So, several nanoparticles including metallic, polymeric, liposomes, lipoproteins, micelles, and emulsions have been reported to yield better results as contrast agents for CT imaging (Cormode et al. 2014; Thomas et al. 2013) Carril et al. worked on 6 nm gold-coated Iron oxide glyco NPs and showed they can be effectively used for multimodal imaging in CT, MRI, and ultrasound (US) as contrast agents. Results explained that the increased gold coating on NPs surface was able to enhance the CT contrast through X-ray attenuation. Moreover, NPs with reduced size, sugar coating and negative surface charge allowed for long circulation time in blood and proved to be biocompatible (Mónica Carril 2014). Additionally, Naha et al. reported the synthesis of a composite consisting of bis-muth–iron oxide nanoparticles (BION) with dextran coating. Data revealed that no cytotoxicity was observed in HepG2 (human liver cancer cell line) and BJ5ta (human fibroblast cell line) after 24 h incubation with NPs. In vivo CT imaging with optimized NPs concentration showed the contrast in heart and blood vessels indicating prolonged circulation half-life. Further, some contrast was observed in liver and spleen suggesting that the non-specific nanoparticle accumulation in these organs. It was concluded that NPs are biocompatible, biodegradable and possess strong X-ray attenuation characteristics, which can be used as a strong contrast agent for dual CT and MRI imaging (Naha et al. 2014). In another attempt, Perlman et al. indicated that IONPs can be used in ultrasonic computed tomography (UCT) for breast imaging. The imaging showed an improvement in contrast to noise ratio and can also serve as a pre-screening platform for disease diagnosis. Moreover, it was suggested that these NPs can be applied for multimodal MRI-ultrasound imaging purposes (Perlman and Azhari 2017). Reguera et al. designed a novel gold–iron oxide-based Janus magnetic-plasmonic NPs as contrast agents for imaging under CT, MRI, PAI, TEM, surface enhanced Raman spectroscopy (SERS) and optical microscopy. These complementary techniques allow obtaining maximum information and can serve as a multipurpose biomedical platform (Reguera et al. 2017).

**Iron oxide nanoparticles in positron emission tomographic imaging**

PET is a nuclear imaging method that provides whole-body imaging and evaluates tissue and organ functions thus enables quantification and localization of activity. However, it cannot reveal anatomical or morphological imaging. So to achieve advancements in imaging, CT, MRI or US can be combined to form a hybrid system such as PET/CT or PET/MRI for better resolution and anatomy of cells and tissues (Evertsson et al. 2017). de Rosales et al. reported the synthesis of a novel NPs system through bifunctional chelator dithiocarbamate–bisphosphonate conjugation to $^{64}$Cu and dextran coated IONPs for PET and MR imaging. Further, the labeling of clinically available IONPs (Endorem/Feridex) with $^{64}$Cu-based bifunctional chelator was performed and their dual-modality imaging was demonstrated in vivo in lymph nodes (Torres Martin de Rosales et al. 2011). Nahrendorf et
al. conjugated a PET tracer $^{64}$Cu to dextran coated magneto fluorescent NPs to yield a tri-modality reporter ($^{64}$Cu-TNP) for PET, MRI and fluorescence imaging. The capability of multimodal NPs was applied to detect macrophages in atherosclerotic plaques. Authors hypothesized that the in vivo PET signal correlates well with the inflammatory plaques observed by MRI, fluorescence imaging and flow cytometry (Nahrendorf et al. 2008). Xiaoqiang et al. developed a multifunctional nanocarrier functionalized with tumor targeting ligand, DOX–conjugated and $^{64}$Cu labeled IONPs. The carrier provides targeted anticancer drug delivery and PET/MRI-based dual imaging modality of tumors expressing integrin $\alpha$, $\beta_3$. In vitro studies explained cRGD ligand (cyclic arginine-glycine-aspartic peptides) conjugated NPs exhibited more cellular uptake and tumor accumulation compared to free NPs shown by quantitative PET imaging and biodistribution analysis (Yang et al. 2011). A similar study was performed by Lee et al. to develop a bifunctional probe for PET and MR imaging. Polyaspartic acid coated IONPs were synthesized and conjugated with a cRGD ligand for integrin targeting and labeled with $^{64}$CuDOTA for PET analysis (Lee et al. 2008). Additionally, Chakravarty et al. synthesized $^{69}$Ge-labeled metal oxides by mixing IONPs with $^{69}$Ge ions. The simple method has an advantage in forming intrinsic radiolabelled NPs without any use of chelators. In addition, these NPs can be used for simultaneous PET and MRI imaging (Chakravarty et al. 2014) (Table 1).

### Bio-sensing applications of iron oxide nanoparticles

#### Role of Iron oxide nanoparticles as nanozymes

Recent developments in nanotechnology have also aimed towards the construction of novel enzyme mimetics (nanozymes) exhibiting biological oxidase, peroxidase, catalase, and superoxide dismutase-like activities (Gao et al. 2017; Karim et al. 2018; Lin et al. 2014d; Shah and Singh 2018). Nanozymes are nanomaterials possessing intrinsic biological enzyme-like properties, which offer several advantages over natural enzymes such as high stability and activity at varying conditions of pH and temperatures, cost effectiveness, easy manipulation and multiple applications on a single platform. The shape, size, and composition controlled synthesis of nanomaterials provides easy modulation of their nanozymatic activity, which is one the major limitations with natural enzymes. Various metal and metal oxide-based nanomaterials such as IONPs, Gold, Silver, Copper, and nanosheets of graphene, MoS$_2$, WS$_2$ are shown to display horseradish peroxidase (HRP)-like activity. These enzyme-mimetic activities are shown to be used for the construction of non-enzymatic biosensors to test the levels/concentrations of glucose, glutathione, cholesterol, H$_2$O$_2$, urea, creatinine and biomarkers for cancer diagnosis (Gawande et al. 2016; Lin et al. 2014a, b; Mahato et al. 2018a, b; Vallabani et al. 2017; Wang et al. 2017; Zheng et al. 2011). These biomolecules are well-known biomarkers for several diseases, thus the developed biosensors could be used for the early diagnosis of these diseases. In general, the peroxidase-like activity of these nanozymes is observed at an optimum pH of 3–5, through the generation of hydroxyl radicals by Fenton reaction. For glucose detection, most of the colorimetric assays follow a two-step procedure. In the first step, glucose gets oxidized in presence of glucose oxidase (G0x) to release H$_2$O$_2$ at neutral pH. In the second step, the obtained H$_2$O$_2$ along with HRP or peroxidase mimetics are allowed to oxidize the substrates like 3,3',5,5'-tetramethylbenzidine (TMB), 2,2',azino-bis(3-ethylbenzothiazoline-6-sulphonic acid) (ABTS) and O-phenylenediamine (OPD) to form the colorimetric product at acidic pH. Although nanozymes degrade H$_2$O$_2$ rapidly and follow the oxidation of the products by hydroxyl radicals, still the reaction suffers from several shortcomings such as lower substrate affinity and specificity than natural enzymes. Such events lead to the lower performance of nanozymes, which ultimately faces limited applicability in sensing and biomedicine. Therefore, it becomes necessary to develop novel ways to enhance the catalytic activity of nanozymes. To address this issue, Yu et al. have studied the impact of citrate, glycine, polylysine, dextran and heparin coating on the peroxidase mimetic MNPs (Yu et al. 2009). They observed that the developed anionic NPs had high affinity towards TMB, whereas cationic NPs showed high affinity for ABTS. Based on the substrate affinity, they were able to detect glucose in the traditional two-step process and suggested that the nanozymatic activity can also be extended to other biomedical applications. Bhagat et al. have developed Gold-core/Cerium oxide-shell NPs exhibiting a multienzyme complex-like activity including catalase, SOD, and peroxidase enzyme-like activities. Kinetic parameter study related to peroxidase activity demonstrated that the core–shell nanozyme activity was comparable to the natural enzyme, horseradish peroxidase (HRP). In addition, authors also explained that oxidation of TMB was carried through electron transfer instead of hydroxyl radical participation. Additionally, the enzyme activity was conserved at a broad range of pH (2–11) and temperatures (up to 90 °C). However, the nanozyme exhibited optimum SOD and catalase activity at neutral pH and for peroxidase, it was found at acidic pH. Finally, the nanozymatic (peroxidase mimetic) activity was utilized for the detection of glucose in a range from 100 μM to 1 mM in a time span of 5 min and at pH 4 (Bhagat et al. 2017). Additionally, Wu et al. developed a magnetic core–shell microgel system with immobilized GOx
| Nanoparticle/material                        | Size (nm) | Applications/results                                                                                                                                                                                                 | References                                      |
|---------------------------------------------|-----------|---------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|------------------------------------------------|
| Ferumoxytol (Feraheme)                      | 17–30     | Treatment for anemia in renal failure patients Used in MR imaging for Stem cell tracking and macrophages. Showed high $T_1$ signal near tumor necrosis regions (can be used for early necrosis detection). Can be effectively used for MR angiography in renal failure patients compared to gadolinium-based contrast agents | Aghighi et al. (2015), Bashir et al. (2015), Castaneda et al. (2011), Hope et al. (2015) and Vasanawala et al. (2016) |
| IONPs coated with HSA, Dopamine and labeled with $^{64}$Cu-DOTA and Cy5.5 | 15        | Used for in vivo tri-modality imaging where MRI used for the study of particle distribution pattern. Under PET imaging showed better signal to noise ratio. NIRF used for both in vivo and ex vivo fluorescence-based imaging | Xie et al. (2010)                              |
| Fluorescent MNPs                            | 10–40     | Used for cell imaging (biological imaging)                                                                                                                                                                            | García et al. (2018)                           |
| JNPs (Au-Fe$_2$C Janus nanoparticles)       | 12        | Applied for triple-modal imaging (in vivo and in vitro) Including MRI, CT, and PAI. Results showed that targeting of NPs was achieved by affibody conjugation (Au-Fe$_2$C-Z$_{HER2:342}$) | Ju et al. (2017)                               |
| Lipophilic Core−Shell Fe$_3$O$_4$@SiO$_2$@Au (Fe$_3$O$_4$ coated with inner silica and Au outer layer) | 157–222   | Results showed targeting of cancer cells through folate receptors. Dual imaging capability for detection of ovarian cancer using MRI, and PAI | Monaco et al. (2017)                           |
| GLUT1-Fe$_3$O$_4$ NPs (Glucose transporter antibody conjugated Fe$_3$O$_4$ NPs) | 10        | Differentiation of infantile hemangiomia from vascular hemangiomia through MRI imaging was realized | Sohn et al. (2015)                             |
| C-ESION (Citrate coated IONPs)              | 3.5–4.5   | For both $T_1$ and $T_2$ contrast imaging, where C-ESION120 used for $T_1$-weighted angiography and C-ESION140 for $T_2$-weighted MRI imaging | Pellico et al. (2017)                          |
| PEG-GdIO (PEGylated Gd-doped iron oxide NPs) | 4.29–4.74 | Showed simultaneous $T_1$–$T_2$ dual-modal MRI imaging and efficient diagnosis of brain gliomas                                                                                                                   | Xiao et al. (2014)                             |
| Fe$_3$O$_4$@GCP                             | 10–22     | Suitable for $T_1$ MRI contrast where $T_1$ weighted images of mice liver were capture with a signal intensity of ~1.2 times more compared to control | Cha et al. (2017)                              |
| Ultra-small IONPs                           | 3–4       | For $T_1$ contrast imaging using MRI                                                                                                                                                                                   | Bao et al. (2018)                              |
| Fe$_3$O$_4$@Au@Glc/CO$_2$H NPs (Gold-Coated Iron Oxide Glyco-nanoparticles) | 6.1       | Can be used as multimodal contrast agent for CT, $T_2$ weighted MRI and US imaging                                                                                                                                   | Mónica Carril (2014)                           |
| BION (Dextran coated bismuth–iron oxide nanohybrid) | 5–15     | Biocompatible and biodegradable NPs used for CT and $T_2$ weighted MRI imaging                                                                                                                                     | Naha et al. (2014)                             |
| Fe$_3$O$_4$                                 | 10        | Used for ultrasonic breast imaging, also be applicable for multimodal MRI-ultrasound imaging                                                                                                                         | Perlman and Azhari (2017)                      |
| Gold-iron oxide NPs                         | 20–50     | Showed potential for multi-purpose imaging such as contrast agent for CT, $T_2$ weighted MRI imaging and PAI                                                                                                           | Reguera et al. (2017)                          |
| $^{64}$Cu-IONPs ($^{64}$Cu and dextran coated IONPs) | 5         | Showed better contrast for in vivo PET-MR imaging                                                                                                                                                                     | Torres Martin de Rosales et al. (2011)         |
| $^{64}$Cu-TNP (IONPs as trireporter NPs)    | 20        | Used for tri-modality NPs system (PET, MRI and fluorescence imaging) for direct detection of macrophages in inflammatory atherosclerosis                                                                                                                                 | Nahrendorf et al. (2008)                       |
and HRP molecules. Due to co-entrapment of enzymes, they utilized the magnetic microgel for the colorimetric detection of glucose in a single step at pH 5.5 (Fig. 3). Moreover, they suggested that this detection system can also be extended for detecting biomolecules through new oxidase or peroxidase platforms (Wu et al. 2015a).

Composite materials have also been studied for the possible nanozymatic activities. In one such attempt, carbon nanotube/polyaniline-based metal oxide (Fe, Co, Ni) NPs are synthesized to show peroxidase mimetic activity using TMB and phenol/4-aminoantipyrine (4-AAP/phenol) to study the peroxidase-like activity and translated into a colorimetric method for glucose detection (Navvabeh Salarizadeh et al. 2017). Additionally, Vazquez-Gonzalez et al., have shown that NPs composed of the Prussian blue (PB), CuFe, FeCoFe, and FeCo inorganic clusters mimic the peroxidase activity. They suggested that PBNPs catalyze the oxidation of NADH by H₂O₂ to form NAD⁺ which can be applied for chemical transformations by NAD⁺ dependent enzymes such as ethanol dehydrogenase (Fig. 4). It was also found that the FeCo NPs catalyzed chemiluminescence generation in presence of H₂O₂ and luminol and extended this system for effective sensing of glucose (Vazquez-Gonzalez et al. 2017).

Recently, bimetallic 2D nanosheets are also reported to act as biological peroxidase enzyme. In this context, Tan et al. synthesized bimetallic nanosheets exhibiting peroxidase-like activity, which can be modulated with the single-stranded DNA (ssDNA). The major attraction of this method was the switchability of peroxidase-like catalytic activity with DNA (Fig. 5). By modulating the enzyme-like activity of these nanosheets they achieved an ultra-sensitive detection of H₂O₂ with a range of 2.86–71.43 nM and comparable detection of glucose with a linear range of 12.86–257.14 µM (Tan et al. 2017).

**Iron oxide nanoparticles in electrochemical sensing and role of biomolecules in enhancing nanozyme activity**

Unlike enzymatic reactions, nanomaterials exhibit the non-enzymatic way to detect the biomolecules. Since these methods are not constrained by the need of special conditions of pH and temperature, the process of detection does not get interference with other comparative biomolecules. Baby and Ramaprabhu et al. reported a superparamagnetic nanocomposite composed of SiO₂ coated Fe₃O₄ NPs dispersed on multiwalled-carbon nano tubes (Fe₃O₄@SiO₂/ MWNT) exhibiting enhanced electron transfer ability and biocompatibility. This system was successfully applied to the development of a glucose and cholesterol sensor without any interference from other biomolecules and did not involve any enzyme (Baby and Ramaprabhu 2011). Further, Nor et al. developed a high sensitive biosensor for glucose
detection using Naftion/GOx/IONPs/screen printed carbon electrode (SPCE). The amperometric biosensor exhibited a wide range of glucose detection with a lower limit of 7 µM (Nor et al. 2017) (Fig. 6). In the similar concept, Kacar et al. developed an amperometric biosensor for creatine monitoring using Fe₃O₄-nanoparticles-modified carbon paste electrodes. The method relies on two enzymatic catalyzed reactions, creatinase, and sarcosine oxidase to generate H₂O₂ and finally, the sensor sensitivity depends on the response towards H₂O₂ for creatine determination (Kacar et al. 2013). Since the creatine level in the human blood and urine acts as a clinical parameter to monitor muscle damage, this system could be of immense benefit to clinical monitoring of these biomolecules.

Composites of multiwalled-carbon nanotubes doped metal oxide NPs (NiO, ZnO, and Fe₃O₄) are coated on glassy carbon electrode and used for the sensitive detection of serotonin from body fluids such as urine. Serotonin is a well-known neurotransmitter and neuromodulator which plays a significant role in several biological processes like liver degeneration, endocrine regulation, anxiety, and depression. Hence, the determination of serotonin levels in the blood can assist to diagnose several diseases. Using this material, authors showed the voltammetry-based determination of serotonin, dopamine and ascorbic acid, simultaneously with high signal to noise ratio (Fayemi et al. 2017). Urea is another marker for kidney failure, obstructions in urinary tract, liver failure and other gastrointestinal problems. Ali et al. devised a potentiometric sensor by immobilizing urease enzyme over chitosan conjugated Fe₃O₄ NPs for detecting urea in the range of 0.1–80 mM (Ali et al. 2013).

Andrea et al. developed IONPs for the sensitive and direct
detection of biomolecules from biological samples. The NPs were functionalized with lipopolysaccharides obtained from a *Brucella* species and detected the presence of *Brucella* antibodies in serum. Further authors suggested that the method is versatile and NPs can be functionalized with different antigens on the surface, which could be used for easy identification of a variety of analytes from the body fluids (Fornara et al. 2008).

To increase the efficiency of nanozymes and overcome the pH constraints, synergistic molecules like nucleobases, nucleosides, nucleotides, and DNA are supplemented in the solution or coated on to the surface of NPs. This synergistic effect allows the design of simple and novel sensors for biomolecule detection at the desired pH (Lin et al. 2014c; Pu et al. 2017; Shah et al. 2015). Thus, to enhance the utility and translate the system into a point-of-care device platform, one-step method of detection is imperative. In this context, Vallabani et al. reported a novel strategy to overcome the limitation of acidic pH for hydroxyl radical generation and showed that with the use of ATP, IONPs exhibited excellent peroxidase mimetic activity at physiological pH. Moreover, the enzymatic activity was preserved over a wide range of pH and temperatures in presence of ATP. They utilized the property for single step detection of glucose at pH 7.4 and further extended to detect glucose level in human blood serum (Vallabani et al. 2017). Further to this study, Liang et al. synthesized novel NPs by growing coordinate polymer (CP) shell made of Fe$^{3+}$ and Adenosine monophosphate (AMP) on Fe$_3$O$_4$ NPs. CP shell showed an advantage in encapsulating a wide variety of guest molecules like nucleic acids, proteins, fluorophores, and NPs. Authors explained that the shell has enhanced peroxidase-like activity due to Fe$_3$O$_4$ present in the core and applied this peroxidase nanozyme for glucose bio-sensing. GOx was entrapped in the shell of Fe$_3$O$_4$ NPs for glucose detection and monitored with a sensitivity of 1.4 µM (Liang et al. 2016). Additionally, Yang et al. reported that adenosine analogs with phosphate groups can enhance the peroxidase-like activity of Fe$_3$O$_4$.
NPs. The improved activity was detected through the oxidation reaction of \( \text{H}_2\text{O}_2 \) and amplex ultra-red reagent generating fluorescence. Here the enhanced peroxidase activity of adenosine phosphate analogs showed the activity trend as \( \text{AMP} > \text{ADP} > \text{ATP} \). Based on the protein adsorption on NPs authors also developed a turn-off system for detection of urinary proteins (Yang et al. 2017) (Table 2).

### Iron oxide nanoparticles in hyperthermia and photo thermal therapy

Hyperthermia is a thermal therapy to produce heat near a local or a systemic tumor by energy sources like microwaves, radio waves, ultrasound energy and magnetism. Recently, it has been realized that the conventional methods of cancer treatment suffer from several limitations such as side effects, drug resistance, low availability of drug at the site of action, fast renal clearance, etc. These challenges have allowed researchers to combine the chemotherapy and radiotherapy with hyperthermia. In magnetic hyperthermia,

| Nanoparticle/material | Size (nm) | Applications/results | References |
|-----------------------|-----------|----------------------|------------|
| Microgel embedded IONP-GOx-HRP | ~ 200 | Exhibited peroxidase like activity. Colorimetric detection of glucose was carried in a single step at pH 5.5 | Wu et al. (2015a) |
| Prussian blue FeCo NPs | 40–50 | PBNPs catalyzed the oxidation of NADH by \( \text{H}_2\text{O}_2 \) to form \( \text{NAD}^+ \) (showed dehydrogenase like activity). FeCo NPs catalyzed chemiluminescence generation in presence of \( \text{H}_2\text{O}_2 \) and luminol (showed Peroxidase like activity). Glucose detection was performed using FeCo NPs | Vazquez-Gonzalez et al. (2017) |
| Cu(HBTC)-I/Fe\(_3\)O\(_4\)-AuNPs nanosheets with ssDNA | 5.99 ± 2.58 | Enhanced TMB oxidation was observed in presence of single stranded DNA. 2D bimetallic immobilized MOF nanosheets were applied for detection of \( \text{H}_2\text{O}_2 \) (2.86–71.43 nM range) and glucose (12.86 to 257.14 \( \mu \text{M} \) range) | Tan et al. (2017) |
| Fe\(_3\)O\(_4\)@SiO\(_2\)/MWNT (SiO\(_2\) coated Fe\(_3\)O\(_4\) NPs dispersed on Multiwalled-carbon nano tubes) | 5–15 | Biosensor was applied for detection of glucose (3 \( \mu \text{M} \)–14 mM range) and cholesterol (10 \( \mu \text{M} \)–4 mM range) | Ramaprabhu (2011) |
| FeNPs@Co\(_3\)O\(_4\) (IONPs loaded in Co\(_3\)O\(_4\) hollow nanocages) | 900 | Applied for glucose detection with a linear range of 0.5–30 \( \mu \text{M} \) (limit of detection was 0.05 \( \mu \text{M} \)) | Zhao (2018) |
| Fe\(_3\)O\(_4\) nanoparticles-modified carbon paste electrodes | – | Creatinine was determined with a detection limit of \( 2.0 \times 10^{-7} \text{ mol L}^{-1} \) | Kacar et al. (2013) |
| Graphene oxide/Fe\(_3\)O\(_4\) nanocomposite | 50 | Biosensor for determination of glucose, with a range of 0.5–10 mM | Wang (2018) |
| MWCNT doped with Ni, Zn, Fe | 10–50 | Serotonin was determined with a detection limit of \( 5.98 \times 10^{-5} \text{ µM} \)–62.8 \( \mu \text{M} \) | Fayemi et al. (2017) |
| Chitosan-IONPs with urease | – | Applicable for the detection of urea | Ali (2013) |
| IONPs | 19.5 | \textit{Brucella} antibodies detection with a detection limit of 0.05 \( \mu \text{g mL}^{-1} \) | Fornara et al. (2008) |
| Fe\(_3\)O\(_4\) NPs | 13 ± 3.5 | ATP-mediated peroxidase like activity of Fe\(_3\)O\(_4\) NPs was observed at pH 7.4. Glucose detection was carried in a single step at physiological pH with a colorimetric detection limit of 50 \( \mu \text{M} \) | Vallabani et al. (2017) |
| Fe\(_3\)O\(_4\) NPs with Fe\(^{3+}\) AMP shell | 10–20 | Glucose detection was demonstrated with a detection limit of 1.4 \( \mu \text{M} \) | Liang et al. (2016) |
| Fe\(_3\)O\(_4\) NPs | ~ 13 | Exhibited peroxidase like activity. Can be applicable as a fluorescent turn-off system for urinary protein detection | Yang et al. (2017) |
the intratumorally injected IONPs generate heating effect after exposing to an external magnetic field and induce the cell death near the tumor zone (Elham Cheraghipour 2012; Kolosnjaj-Tabi and Wilhelm 2017). Due to poor cellular architecture, cancer cells are very prone to be damaged by the slight increase in the surrounding temperature. Additionally, using hyperthermia strategy, the temperature of the surrounding environment can be increased up to 55–60 °C, which can be very well withstood by normal healthy cells, but not by cancerous cells. Moreover, IONPs can be used to prepare synergistic nano-hybrids tuned for magnetic hyperthermia and photothermia. Photothermal therapy is also possible with the use of other nanoparticles such as anisotropic nanostructures of gold, copper, silver, carbon nanotubes, and graphene NPs (Boca et al. 2011; He et al. 2014; Liu et al. 2007; Yavuz et al. 2009). Other morphologies of IONPs are also developed for the photothermal treatment of diseases. Espinosa et al. have used nanocubes of IONPs and showed that when these nanocubes are exposed to the magnetic field as well as near-infrared laser irradiation, two- to five fold amplification in the production of heat was generated than when used magnetic field alone (Fig. 7). Moreover, it was demonstrated the dual-mode stimulation generated efficient heat with low iron concentration (0.25 M) and acceptable laser power irradiation (0.3 W/cm²) and resulted in a complete cell death and solid tumor suppression (Espinosa et al. 2016). In another attempt, Niu et al. developed a nanosystem comprising of IONPs (Fe$_3$O$_4$), indocyanine green (ICG) and perfluoropentane (PFP) encapsulated in poly (lactideco-glycolide) (PLGA) nanoparticles for NIR induced PTT. The experiments with MCF-7 tumors in mice showed that these multifunctional NPs can enhance tumor ablation upon NIR laser irradiation and can act as a key photothermal agent against the tumors (Niu et al. 2017).

Addressing hyperthermia, Mazario et al. synthesized 10 nm sized MNPs functionalized with HAS protein and the experimental data revealed these functional materials have the potential role in mediating magnetic hyperthermia by enhancing the temperature of cancer cells. Moreover, authors suggested that heating could induce irreversible damage to cellular proteins and enzymes and thereby the regulation of apoptosis in cells and tissues (Mazario 2017). In a related study, Shen et al. synthesized a magnetic nanocluster for PTT using near-infrared light irradiation. They found that after radiation exposure clusters of Fe$_3$O$_4$ produced more heating thereby impart significant cytotoxic to A549 cells (human lung carcinoma) compared to bigger sized Fe$_3$O$_4$ NPs. The mechanistic studies revealed the cell death was caused due to apoptosis, but not necrosis. Further, in vivo studies demonstrated that these clusters can be applied for promising tumor treatment through PTT (Fig. 8) (Shen et al. 2015). Chen et al. have developed highly crystalline IONPs...
(HCIONPs) coated with the anti-biofouling polymer and used then for photothermal cancer therapy. Results revealed NPs were effectively accumulated in the tumor site of SUM-159 tumor-bearing mouse though permeability and retention effect. Further laser irradiation exhibited complete tumor regression within 3 weeks compared to control. Authors suggested that enhanced PTT was due to high crystalline and preferred lattice plane orientations of as prepared HCIONPs compared to normal Fe₃O₄ NPs (Hongwei Chen 2014).

Multifunctional IONPs are also designed and have shown better results than their uni-functional counterparts. In this context, PEGylated Fe/Fe₃O₄ NPs have been developed for exhibiting triple functions comprising PTT, targeting, and MRI (Fig. 9). Targeting of cells was achieved with neodymium magnet placed beside a xenograft tumor developed from HeLa cells. The multi-modality allowed the NPs to accumulate in the tumor region, therefore, exhibited intense MRI signal with high photothermal activity (Zhou et al. 2014). PEG coating on nanoparticle surface imparts biocompatibility and avoidance to the reticuloendothelial system (RES), which renders the long-term circulation in blood plasma (Larson et al. 2012). Therefore, biocompatible nanomaterials would be an ideal candidate.

Table 3  Summary of iron oxide based nanoparticles for hyperthermia and photo thermal therapy

| Nanoparticle/material | Size (nm) | Applications/results | References |
|-----------------------|-----------|----------------------|------------|
| IONPs (nano-cubes)    | 20        | The dual mode (hyperthermia and PTT) of treatment amplified the heating effect by two- to fivefold in comparison with magnetic stimulation alone. Results showed that in both in vitro (SKOV3) (ovarian cancer), PC3 (prostate cancer) and A431 (epidermoid cancer) and in vivo (A431 cancerous cells were injected in nude NMRI mice) complete cell death was observed after dual mode exposure | Espinosa et al. (2016) |
| ICG/Fe₃O₄ loaded PLGA NPs | Fe₃O₄: 10  | Used as an efficient treatment by PTT. In vitro treatment of NPs to MCF-7 breast cancer cells confirmed the damage to cells and in vivo studies demonstrated IONPs can be used as an effective agent for tumor ablation | Niu et al. (2017) |
| Carboxyl-amine functionalized SPIONs based ferrofluids | ~ 20       | In vitro hyperthermia studies revealed terephthalic acid (TA) and aminoterephthalic acid (ATA) coated SPIONs induced ~ 90% cell death in breast cancer cells (MCF-7) | Kandasamy (2018a) |
| IONPs with HSA        | 10        | Used for thermal therapy. MNPs exhibited a saturation magnetization of 63 emu g⁻¹ at 310 K and produced a localized heat in presence of an alternating magnetic field | Mazario (2017) |
| Clustered magnetic Fe₃O₄ NPs | Fe₃O₄: 15  | Used for PTT. The clustered NPs induced high temperature and proved to be more cytotoxic against A549 cells both in vitro and in vivo | Shen et al. (2015) |
| SPIONS                | 6–10      | Hyperthermia based thermotherapy for liver cancer treatment | Kandasamy (2018b) |
| Crystallized IONPs (HCIONPs) | 15        | Showed effective PTT against SUM-159 tumor-bearing mice | Hongwei Chen (2014) |
| PEGylated Fe@ Fe₃O₄ (PEGylated iron/iron oxide core/shell NPs) | 13.4 ± 0.8 | These multifunctional NPs can be applied for targeting, MRI imaging and PTT | Zhou et al. (2014) |
| Fe₃O₄@CMCT (carboxymethyl chitosan stabilized Fe₃O₄ NPs) | 177       | Used for PTT. NPs were found accumulated in the mice tumor region and PTT induced the increase in temperature up to ~ 52 °C | Shen et al. (2013) |
for multifunctional applications cell targeting, MRI, sensing, hyperthermia, and PTT. For instance, Shen et al. synthesized a carboxymethyl chitosan coated Fe₃O₄ NPs, which exhibited extremely low toxicity and high PTT efficiency. Furthermore, they stated that these NPs platform can be easily fabricated for multiple applications (Shen et al. 2013) (Table 3).

**Iron oxide nanoparticles as delivery agents**

**Drug delivery applications**

Effective treatment of cancer still remains a major challenge in medicine due to several problems such as drug/multidrug resistance, lack of selective targets for a tumor (El-Boubbou 2018; Vasir and Labhasetwar 2005). Nanotechnology has recently shown some success in effective cancer treatment due to the unusual properties of materials. Among several NP types, IONPs have gained the most attention for applications in nanomedicines due to some of the key attributes, including stable colloidal suspension, resistance to in vivo degradation, presence of large surface area to graft targeting moieties, high payload delivery of drugs, synergistic activity in improving the sensitivity of drugs towards cancer treatment, and reversing the resistance of cancerous cells (Bahrami et al. 2017; Ulbrich et al. 2016).

Traditional methods of cancer treatment include surgery, chemotherapy, radiotherapy, and combinational therapy to alleviate the tumors. However, damage to surrounding cells around a tumor and radio-resistance of cells limits the effectiveness of these conventional therapies. The multifunctional nature of IONPs has been recently exploited for the effective drug delivery for cancer and other disease treatment. Pirayesh Islamian et al. used superparamagnetic mesoporous hydroxyapatite conjugated doxorubicin and deoxy-D-glucose nanocomposites to boost breast cancer chemo and radiotherapy (Pirayesh Islamian et al. 2017). They worked on SKBR3 and T47D breast cancer cell culture models and reported that the cell viability was significantly decreased with combined nanocomposite effect compared to the radiotherapy alone. Mechanistically, they found that targeting of breast cancer cell was achieved with deoxy-d-glucose moiety conjugated on IONPs surface and doxorubicin acted as therapeutic agent, thus the combined effect leads to the improved breast cancer radiotherapy by increased localization of NPs. When investigated further, it was found that the extent of cytotoxicity in tumor cells was much more, with minimum side effects and damage to normal healthy cells. In another strategy, Ye et al suggested that Fe₃O₄ NPs can increase the efficacy of cryoablation; a process uses extreme cold conditions to treat cancerous cells. Their data indicated that Fe₃O₄ NPs altered intracellular ice formation ability during freezing, recrystallization, and thawing, which leads to the enhanced killing of MCF-7 cells. Therefore, the idea of enhanced ablation using IONPs can be successfully applied to effectively treat tumors in near future (Ye et al. 2017).

Cisplatin is platinum-based anticancer agent reported to treat various types of cancers including lung, testicular, bladder, ovarian, breast, and brain tumors (Dasari and Tchounwou 2014). However, the excess usage of cisplatin is also reported to exhibit various side effects such as kidney damage, neurotoxicity, bone marrow suppression, heart diseases, and allergic reactions (Barabas et al. 2008). It is also well known that the drug resistance shown by tumor cells limits their probability of clinical trial success. To overcome these limitations, platinum drugs are suggested to be encapsulated into polymers or loaded into multifunctional nanocomposites for effective treatment of cancers. In this context, Yan Zhang et al. fabricated a nanocomposite comprising of Fe₃O₄ core and polymeric inner shell covered with PEG, and folic acid, and the cisplatin was encapsulated into the inner shell through coordination of amino groups (Yan Zhang 2014). The in vitro release kinetics of cisplatin showed better release at acidic pH (pH ~ 4.5) and resulted in a cytotoxic response in HeLa cells through ligand-mediated targeting of folic receptors (overexpressed on HeLa cells) (Fig. 10). Additionally, Ebrahim et al. have developed a PLGA-PEG copolymer system by emulsion method, which encapsulated Fe₃O₄ NPs with doxorubicin (DOX) drug. With the controlled DOX release in tumor cells, this
biodegradable nanocomposite was designed to minimize the drug uptake in normal cells and also to control the drug amount and targeting via copolymer coated IONPs and pH. The results revealed that the drug release was high at acidic pH and found effective as a chemopreventive and chemotherapeutic agent for effective treatment of lung and other solid tumors (Ebrahimi 2014a, b).

Epidermal growth factor receptor (EGFR) is also a well-known targeting moiety, which has been well-explored for the targeted drug delivery in cancer cells. Utilizing this strategy, Xupeng et al. have developed a multifunctional nanocomposite consisting of IONPs and shown applications in the diagnosis, targeting, and chemo and photothermal therapy of cancer (Xupeng Mu 2017). The nanocomposite was designed by conjugating EGFR antibody on polydopamine-coated Fe3O4 NPs and loaded with DOX. This nanocomposite exhibited pH and NIR triggered drug release, which resulted in effective inhibition of colon cancer cells (DLD-1, exhibiting overexpression of EGFR) due to synergistic chemo and photothermal therapy. Additionally, these nanocomposites were also utilized for T2 contrast generation to follow the tumor growth by MRI scanning under in vivo experimental condition. In another attempt, Arachchige et al., synthesized dextran coated IONPs and conjugated them with DOX and fluorescein isothiocyanate (Fig. 11). The so produced IONPs laid an efficient combination platform for imaging through Fe3O4 contrast (MRI), red fluorescence (auto fluorescing DOX) and green fluorescence (fluorescein isothiocyanate). Results revealed that significant drug internalization was obtained in pancreatic cancer cells (MIA PaCa-2 cells). Further, the dual-fluorescent tracking mode showed that the DOX was cleaved from the NPs and accumulated at the targeting site (nucleus). Such strategies could also be utilized for conjugation of an additional antibody to the existing NPs platform, which could be helpful in a tumor specific therapy (Arachchige et al. 2017).

Jia et al. constructed a nanocarrier with PLGA polymer encapsulating IONPs and DOX. The drug internalization study was performed in multiple cancer cell culture models such as Lewis lung carcinoma (LLC), human osteosarcoma (OS-732), and murine-leukemic monocyte–macrophage (RAW 264.7) cell lines and results revealed that IONPs-DOX combination was internalized in cells in higher amount with respect to when DOX alone was used. In addition, a higher concentration of IONPs-DOX internalization induced apoptosis in LLC cell line. Under In vivo experiments, results showed that more anti-tumor effect was seen with combination therapy, which was further improved in presence of external magnet (Jia et al. 2012).

Fig. 11 Synthesis and functionalization of superparamagnetic iron oxide (SPIO) nanoparticles for rapid cellular entry and release of the cancer drug Doxorubicin (DOX) in human pancreatic cancer cells. Dextran coated Fe3O4 core with DOX (red fluorescence) and FITC (green fluorescence) surface conjugation chemistry, and the rapid entry (15 min) and intracellular release and accumulation of the cancer drug in the nucleus (white arrow head) of human pancreatic cancer Mia Paca-2 cells. Reprinted with permission from ref (Arachchige et al. 2017) Copyright (2017) Elsevier
The blood–brain barrier is a semipermeable membrane that protects neural tissue from toxins and exogenous substances. The tight junctions in the endothelial cells around the capillaries are responsible for the barrier formation. Daunorubicin (DNR) is a potent topoisomerase inhibitor and used as an effective chemotherapeutic agent to treat leukemia and neuroblastoma. Xuhua et al. synthesized DNR loaded Fe₃O₄ NPs and found the formulation was efficient enough to cross the blood–brain barrier which separates the circulating blood from the brain. Results suggested that the combination therapy can trigger apoptosis in glioma cells and thus used as a promising agent to cross the otherwise impermeable blood–brain barrier and treat brain tumors (Xuhua Mao 2016). Experimental data indicated that the formulation increased the barrier permeability through opening tight junctions via controlling the expression of cell–cell adhesion proteins (E-cadherin, ZO-1, and Claudin-1). Homoharringtonine (HTT) conjugated Fe₃O₄ NPs were synthesized by Chen et al. to inhibit leukemia. Results showed NPs and drug combination enhanced the inhibitory effect on myeloid leukemia cell lines compared to HTT exposure alone. They found cell death was caused due to apoptosis and observed cell cycle arrest at G0/G1 phase. Moreover, in vivo studies explained the combination worked efficiently to decrease the tumor volume compared to drug alone (Chen et al. 2016). A similar study explained the combination of Fe₃O₄ with adriamycin or daunorubicin drugs showed a potential inhibitory effect on lymphoma. A detailed study on Raji cells explained that the inhibition was due to induction of apoptosis which was further enhanced in the presence of NPs (Hongmei Jing 2010). Huilan et al. designed a nanocomposite encompassing Fe₃O₄ NPs and an anticancer drug ursolic methyl ester. They demonstrated combination treatment increased the rate of apoptosis in drug-resistant human leukemia cells (KA cells) compared to the drug alone. The authors suggested that this approach to inhibit the growth of drug-resistant cancer cells can be used as an alternative method to treat other cancers as well (Huilan Yue 2016).

Osteoporosis is a condition where bones become weak and brittle due to an imbalance between osteoblasts and osteoclasts (OCs). Thus, reducing the OCs activity, which involves the breakdown of bone tissues, can improve the bone damage. To overcome the effect a composite nanosystem was developed using Fe₃O₄ NPs with alendronate drug for treating osteoporosis. In this novel strategy, after the delivery of NPs near osteoclasts (OCs) cells, a dose of radiofrequency was applied to induce thermolysis to OCs. It was also suggested that these multifunctional NPs with their drug delivery, thermolysis, and contrast (MRI) generation ability can be used as a potential therapeutic and imaging agent for osteoporosis (Lee et al. 2016).

**Gene delivery applications**

Gene delivery is a therapeutic technique for the delivery of nucleic acids instead of drugs or surgery to treat diseases. In general, it is a great challenge to deliver biological drugs like siRNA, and plasmid DNA to target cells or tissues without being damaged by nucleases. Therefore, to overwhelm the damage, nanocarriers like IONPs have been used to transport the genes and release at the intended target sites (Kievit and Zhang 2011). Borroni et al. developed a novel vector that can deliver therapeutic genes for treating tumors. The gene-carrier contained IONPs conjugated with lentiviral vectors to deliver target gene at the area of interest (Fig. 12). To check the efficiency, this nanocarrier was injected with a reporter GFP gene (green fluorescent protein) into a tumor bearing mice and found sustained gene expression near the target areas. Their data suggest that in future LV-MNPs can be successfully tailored to deliver therapeutic genes for selectively inhibiting the growth of tumors (Borroni et al. 2017). Additionally, Mahajan et al. designed a novel IONPs carrier to stop the progression of pancreatic cancer. IONPs were coupled with siRNA (siPLK1) directed against Polo-like kinase-1 (cell cycle-specific serine-threonine-kinase). Moreover, siPLK1-IONPs were conjugated to membrane translocation peptide (myristoylated polyarginine peptides (MPAP)) for driving endosomal escape and mediating transport to the cytoplasm and a tumor-selective peptide underglycosylated MUC1 (uMUC1)-specific peptide (EPPT1) to increase intracellular and tumor-specific delivery. The
experimental data revealed the significant accumulation of NPs and resulted in efficient PLK1 silencing that leads to tumor suppression through increased apoptosis (Mahajan et al. 2016).

Cheong et al. synthesized IONPs-based carrier loaded with water-soluble chitosan and linoleic acid (SCLNs) for targeting hepatocytes. Authors confirmed the NPs localization in the liver cells by injecting a nuclear isomer (Technetium-99m) labeled SCLNs in mice using nuclear and magnetic resonance imaging. Further SCLN/enhanced GFP (pEGFP) complexes transfected in primary hepatocytes, intravenous administration in mice showed a significant increase in GFP expression. In addition, the gene silencing was effectively achieved by injecting SCLN complexes containing specific siRNA into mice. Thus, the results suggested that SCLNs can be used as a useful platform for imaging and gene delivery simultaneously (Cheong et al. 2009).

In addition, Ling-Feng et al. evaluated the use of IONPs as ideal gene-carrier for PTEN (Phosphatase and tensin homolog) gene delivery to reverse cisplatin-resistance in lung cancer. PTEN acts as a tumor suppressor gene and its inactivity causes the development of several cancers. A549/CDDP (cisplatin-resistant) cells were transfected with wild PTEN gene expression plasmid (pGFP-PTEN) using IONPs and liposomes as carriers. It was observed The IONPs mediated PTEN transfection showed higher efficiency and more PTEN expression compared to empty liposome-mediated transfection. Further, PTEN transfection increased the apoptotic cell population and enhanced the sensitivity of A549/CDDP cells to cisplatin indicating PTEN can be an effective target against cisplatin-resistant lung cancer cells (Ling-feng Min 2012) (Table 4).

**Iron oxide nanoparticles as broad spectrum antimicrobial agent**

Although IONPs have shown tremendous applications in drug delivery, phototherapy, and chemotherapy, they have also found overarching potential as the antimicrobial and antifungal agent. In the concept of drug resistance in microbes, the developments of new drugs or novel strategies for efficient destruction of these pathogens need immediate attention. It is well known that antimicrobial resistance poses a catastrophic threat to humans because if it continues to grow with the current pace for 20 more years, it is estimated that people visiting hospitals for even minor surgery may die due to an ordinary microbial infection, which cannot be treated by antibiotics. It is estimated that the number of deaths due to microbial infection would surpass the mortality due to cancer or diabetes in few decades. Therefore, novel antimicrobials are needed to avoid these circumstances in near future. Nanomaterials offer several advantages over traditional antibiotics as effective antimicrobials, as microbes may not be able to develop resistance against these inorganic materials, therefore, it is expected that the antimicrobial activity of nanomaterials would remain same, even after multiple uses, which is one of the biggest limitations with antibiotics. Among nanomaterials, IONPs are well explored as an effective antimicrobial candidate. Studies on IONPs showed potential antimicrobial activity and literature studies revealed citrate coated Fe3O4 NPs have an inhibitory effect on *Escherichia coli*, *Bacillus subtilis*, *Candida albicans*, *Aspergillus niger* and *Fusarium solani* (Arakha et al. 2015; Nehra et al. 2018). Further, Patra et al. applied green synthesis for the synthesis of Fe3O4 NPs from corn plant extract and explained that NPs exerted a synergistic antibacterial and antifungal activity (Patra et al. 2017). In another attempt, a green chemistry approach using *Couroupita guianensis* fruit extract was applied to synthesize Fe3O4 NPs and the particles exhibited potent bactericidal action on several human pathogens (Gao et al. 2017). Additionally, Ismail et al. synthesized IONPs (α-Fe2O3) and determined their antibacterial activity against Gram-positive and Gram-negative bacteria and stated that IONPs can capture *Staphylococcus aureus* through magnetic field effect (Ismail et al. 2015). Arokiyaraj et al. have developed IONPs treated with *Argemone mexicana* L. leaf extract and showed a significant colony growth inhibition against *Escherichia coli* and *Proteus mirabilis* (Arokiyaraj 2013). As discussed above, more strategies could be devised to develop synergistic IONPs platform, which can be used as a carrier system to treat microbial diseases in future.

**Summary and future perspectives**

IONPs with their magnetic characteristics and contrast have already successfully applied in areas of biomedicine, including diagnostics as a probe (MRI scanning) for detection of diseases or disorders in the brain, cardiovascular, liver, blood vessels and other vital organs. Moreover, with advancements, IONPs are prepared in combinations to achieve multiple functions in a single stage like T1 and T2 MRI, and PET/CT/NIRF/MRI/PA imaging. Recently IONPs-based nanohybrids were tuned for hyperthermia and PTT, where even low concentrations are capable to enhance the heat generation at the tumor site and can be efficiently used for cellular therapies. In bio-sensing, advances in Nanohybrid IONPs synthesis paved a path to introduce enzyme mimetics, possessing peroxidase, oxidase, and catalase-like activities. In addition, the nanohybrids or conjugated NPs simplified the detection of biomolecules in a single step and laid the foundation to create novel nano-sensors and nano-devices. Further to overcome the obstacles in cancer and multi-drug resistant
| Nanoparticle/material | Size (nm) | Applications/results | References |
|----------------------|-----------|-----------------------|------------|
| IONPs coated with 2-deoxy-d-glucose and DOX | Pore size: 12 | NPs enhanced chemo-radiotherapy efficiency in breast cancer cells through targeting. Results showed the combined NPs treatment with doxorubicin and 2-deoxy-D-glucose boosted the breast cancer cure through improved radiotherapy | Pirayesh Islamian et al. (2017) |
| Fe$_3$O$_4$ NPs | 9 | Used for treating tumors through cryoablation therapy. Results indicated MCF7 cells were killed efficiently by cryoablation | Ye et al. (2017) |
| Fe$_3$O$_4$ NPs @PEG, folate and cisplatin (Folic acid-Polymer conjugated Fe$_3$O$_4$ NPs with cisplatin) | ~10 | Used for ligand-mediated targeting and chemotherapy. Cisplatin-loaded NPs showed concentration dependent cytotoxicity in HeLa cells. Moreover folate conjugation exhibited more cytotoxicity compared to non-conjugated NPs | Yan Zhang (2014) |
| DOX encapsulated Fe$_3$O$_4$ | ~12 | Used as a nano-carrier for anticancer drugs like doxorubicin. NPs can be applied as a chemotherapeutic system for treating lung cancers | Ebrahimi et al. (2014a, b) |
| Polydopamine coated Fe$_3$O$_4$ with EGFR antibody and DOX | ~60 | Used as a multifunctional composites in diagnosis (MRI imaging) and cancer treatment (chemo-photo thermal therapy). Results showed the combination therapy is efficient enough in killing EGFR expressed tumor cells (colon cancer) | Xupeng Mu (2017) |
| Dextran coated IONPs with FITC and DOX | ~8 | Used for drug delivery with multimodal imaging (MRI and FITC Fluorescence) and cancer treatment (drug and hyperthermia). Can be applied for treating pancreatic cancers | Arachchige et al. (2017) |
| MNPs encapsulated in PLGA with DOX | MNPs: 4–6, DOX-MNPs: 200–300 | Used as a nano-carrier for drugs like doxorubicin. Results showed DOX-MNPs were internalized in to lung cancer cells (Lewis lung carcinoma cells) and induced apoptosis. Moreover in vivo studies revealed more anti-tumor activity in presence of an external magnetic field | Jia et al. (2012) |
| DOX loaded Fe$_3$O$_4$-reduced graphene oxide | 8–10 | Showed maximum inhibition of HeLa cells with hyperthermia assisted treatment | Gupta (2018) |
| Daunorubicin loaded Fe$_3$O$_4$ NPs | 100 | Used to treat brain glioma. Results showed this drug loaded NPs can be efficiently delivered into blood brain barrier and can act as promising drug to treat blood tumors | Xuhua Mao (2016) |
| Homoharringtonine conjugated Fe$_3$O$_4$ NPs | 11.2 | Used for in vitro and in vivo chemotherapy towards hematological malignancy. Results indicated drug conjugated MNPs injected in tumor bearing mice (leukemia) showed a significant decrease in tumor growth compared to drug treatment alone | Chen et al. (2016) |
diseases, multifunctional IONPs were being designed for diagnosis, targeting, nanocarrier, chemo and phototherapy agents. In conclusion, more progression in the novel synthesis of nanocomposites with multifunctional modalities can find better ways to use IONPs as nano-theranostic entities in biomedicine. The future of IONPs in biomedical applications holds great promise especially in the area of disease diagnosis, early detection, cellular and deep tissue imaging, drug/gene delivery as well as multifunctional therapeutics. Although, Feraheme (US FDA approved) is being used by the consumers, more of such IONPs-based materials need to be researched and made available to the consumer market. The current emphasis of molecular medicine is to develop more novel tools, which can be used for early-stage disease diagnosis and more of point-of-care diagnostics. Integration of nanomaterials, especially IONPs, could extend the construction of the theranostic platform, which combines therapeutics with diagnostics. Such attempts would primarily make the diagnosis processes simpler, speedier and less invasive. Personalized medicine is also gaining attention and it is expected that the integration of nanotechnology could result in overarching outcomes. In coming years, multifunctional IONPs would be an attractive material for biomedical applications and may change the usual business model of pharmaceutical industries.

Acknowledgements The financial assistance for the Centre for Nanotechnology Research and Applications (CENTRA) by The Gujarat Institute for Chemical Technology (GICT) and the funding from the Department of Science and Technology-Science and Engineering Research Board (SERB) (Grant no.: ILS/SERB/2015-16/01) to Dr Sanjay Singh under the scheme of Start-Up Research Grant (Young Scientists)—Life Sciences are gratefully acknowledged. Dr Singh is also thankful for the financial support provided by the Ahmedabad University as Seed Grant (AU/SG/SAS/DBLS/17-18/03).
Compliance with ethical standards

Conflict of interest The authors declare no conflict of interest.

Open Access This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made.

References

Aghighi M, Golovko D, Ansari C, Marina NM, Pisani L, Kurlander L, Klenk C, Bhaumik S, Wendland M, Daldrop-Link HE (2015) Imaging tumor necrosis with ferumoxytol. PLoS One 10(1):e0142665. https://doi.org/10.1371/journal.pone.0142665

Ali A, Atif M, Anees AA, Ansari MQ, Israr MQ, Sadaf JR, Ahmed E, Nur O, Willander M (2013) Potentiometric urea biosensor utilizing nanobiocomposite of chitosan-iron oxide magnetic nanoparticles. J Phys Conf Ser. https://doi.org/10.1088/1742-6596/41/1/012024

Arachchige MP, Laha SS, Naik AR, Lewis KT, Naik R, Jena BP (2017) Functionalized nanoparticles enable tracking the rapid entry and release of doxorubicin in human pancreatic cancer cells. Micron 92:25–31. https://doi.org/10.1016/j.micron.2016.10.005

Arakha M, Pal S, Samantarrai D, Panigrahi TK, Mallick BC, Pramanik K, Mallick B, Jha S (2015) Antimicrobial activity of iron oxide nanoparticle upon modulation of nanoparticle-bacteria interface. Sci Rep 5:48183. https://doi.org/10.1038/srep48183

Arokiyaraj S, Udaya Prakash MS, Valan Arasu M, Vijayakumar B, Vincent S (2013) Enhanced antibacterial activity of iron oxide magnetic nanoparticles treated with Argemone mexicana L. leaf extract: an in vitro study. Mater Res Bull 48:3323–3327. https://doi.org/10.1016/j.materresbull.2013.05.059

Baby TT, Ramaprabhu S (2011) Non-enzymatic glucose and cholesterol biosensors based on silica coated nano iron oxide dispersed multiwalled carbon nanotubes. Int Conf Nanosci Technol Soc Implications. https://doi.org/10.1109/NNSTS.2011.6111981

Bahrami B, Hojat-Farsangi M, Mohammad H, Anvari E, Ghalamfarsa G, Yousefi M, Jadidi-Niaragh F (2017) Nanoparticles and targeted drug delivery in cancer therapy. Immunol Lett 190:64–83. https://doi.org/10.1016/j.imlett.2017.07.015

Bao Y, Sherwood JA, Z S (2018) Magnetic iron oxide nanoparticles as T1 contrast agents for magnetic resonance imaging. J Mater Chem C 6:1280–1290. https://doi.org/10.1039/C7TC05854C

Barakas K, Milner R, Lurie D, Adin C (2008) Cisplatin: a review. Vet Comp Oncol 6(1):1–18. https://doi.org/10.1111/j.1476-5829.2007.00142.x

Bashir MR, Bhatti L, Marin D, Nelson RC (2015) Emerging applications for ferumoxytol as a contrast agent in MRI. J Mag Reson Imaging 41(4):884–898. https://doi.org/10.1002/jmri.24691

Bhatg S, Srikanth Vallabani NV, Shuttanandan V, Bowden M, Karakoti AS, Singh S (2017) Gold core/ceria shell-based redox active nanozyme mimicking the biological multienzyme complex phenomenon. J Colloid Interface Sci 513:831–842. https://doi.org/10.1016/j.jcis.2017.11.064

Boca SC, Potara M, Gabudean AM, Juhem A, Baldeck PL, Astilean S (2011) Chitosan-coated triangular silver nanoparticles as a novel class of biocompatible, highly effective photothermal transducers for in vitro cancer cell therapy. Cancer Lett 311(2):131–140. https://doi.org/10.1016/j.canlet.2011.06.022

Borroni E, Miola M, Ferraris S, Ricci G, Zuzek Rozman K, Kostevsek N, Catizone A, Rimondini L, Prat M, Verne E, Follenzi A (2017) Tumor targeting by lentiviral vectors combined with magnetic nanoparticles in mice. Acta Biomater 59:303–316. https://doi.org/10.1016/j.actbio.2017.07.007

Cai Y, Cao C, He X, Yang C, Tian L, Zhu R, Pan Y (2015) Enhanced magnetic resonance imaging and staining of cancer cells using ferrimagnetic H-ferritin nanoparticles with increasing core size. Int J Nanomed 10:2619–2634. https://doi.org/10.2147/IJN.S80025

Castaneda RT, Khurana A, Khan R, Daldrup-Link HE (2011) Labeling stem cells with ferumoxytol, an FDA-approved iron oxide nanoparticle. J Vis Exp (57):e3482. https://doi.org/10.3791/3482

Cha R, Li J, Liu Y, Zhang Y, Xie Q, Zhang M (2017) Fe3O4 nanoparticles modified by CD-containing star polymer for MRI and drug delivery. Colloids Surf B Biointerfaces 158:213–221. https://doi.org/10.1016/j.colsurfb.2017.06.049

Chakravarty R, Valdivinos HF, Chen F, Lewis CM, Ellison PA, Luo H, Meyerand ME, Nickles RJ, Cai W (2014) Intrinsically germanium-69-labeled iron oxide nanoparticles: synthesis and in-vivo dual-modality PET/MRI imaging. Adv Mater 26(30):5119–5123. https://doi.org/10.1002/adma.201401572

 Chen Z, Yin JJ, Zhou YT, Zhang Y, Song L, Song M, Hu S, Gu N (2012) Dual enzyme-like activities of iron oxide nanoparticles and their implication for diminishing cytotoxicity. ACS Nano 6(5):4001–4012. https://doi.org/10.1021/nn300291r

Chen M, Xiong F, Ma L, Yao H, Wang Q, Wen L, Wang Q, Gu N, Chen S (2016) Inhibitory effect of magnetic Fe3O4 nanoparticles coloaded with homoharringtonine on human leukemia cells in vivo and in vitro. Int J Nanomed 11:4413–4422. https://doi.org/10.2147/IJN.S105543

Cheong SJ, Lee CM, Kim SL, Jeong HJ, Kim EM, Park EH, Kim DW, Lim ST, Sohn MH (2009) Superparamagnetic iron oxide nanoparticles-loaded chitosan-linoleic acid nanoparticles as an effective hepatocyte-targeted gene delivery system. Int J Pharm 372(1–2):169–176. https://doi.org/10.1016/j.ijpharm.2009.01.009

Cormode DP, Naha PC, Fayad ZA (2014) Nanoparticle contrast agents for computed tomography: a focus on micelles. Contrast Media Mol Imaging 9(1):37–52. https://doi.org/10.1002/cmmi.1551

Dasari S, Tchounwou PB (2014) Cisplatin in cancer therapy: molecular mechanisms of action. Eur J Pharmacol 740:364–378. https://doi.org/10.1016/j.ejphar.2014.07.025

de Rosales TM, Tavare R, Paul R, Jauregui-Osoro RL, Protti M, Gloria A, Varma A, Sandza G, Blower IJP (2011) Synthesis of 64Cu(II)-bis(dithiocarbamatebisphosphate) and its conjugation with superparamagnetic iron oxide nanoparticles: in vivo evaluation as dual-modality PET-MRI agent. Angew Chem Int Ed Engl 50(24):5509–5513. https://doi.org/10.1002/anie.201007894

Ebrahimi E, Akbarzadeh A, Abbasi E, Khandaghi AA, AbasaliZadeh F, Davaran S (2014a) Novel drug delivery system based on doxorubicin-encapsulated magnetic nanoparticles modified with PLGA-PEG1000 copolymer. Artif Cells Nanomed Biotechnol. https://doi.org/10.3109/21691401.2014.944646

Ebrahimi E, Khandaghi AA, Valipour F, Babaie S, Asghari F, Motaii S, Abbasi E, Akbarzadeh A, Davaran S (2014b) In vitro study and characterization of doxorubicin-loaded magnetic nanoparticles modified with biodegradable copolymers. Artif Cells Nanomed Biotechnol. https://doi.org/10.3109/21691401.2014.968822

El-Boubbou K (2018) Magnetic iron oxide nanoparticles as drug carriers: clinical relevance. Nanomedicine (Lond). https://doi.org/10.2217/nnm-2017-0336

Elham Cheraghipour SJ, Mehdizadeh AR (2012) Citrate capped superparamagnetic iron oxide nanoparticles: characterization of doxorubicin-loaded magnetic nanoparticles modified with PLGA-PEG1000 copolymer. Artif Cells Nanomed Biotechnol. https://doi.org/10.3109/21691401.2014.944646

Elham Cheraghipour SJ, Mehdizadeh AR (2012) Citrate capped superparamagnetic iron oxide nanoparticles used for hyperthermia therapy. J Biomed Sci Eng 5:715–719. https://doi.org/10.4236/jbise.2012.512089
Emily A. Waters SAW (2008) Contrast agents for MRI. Basic Res Cardiol 103(2):114–121. https://doi.org/10.1007/s00395-008-0711-6

Espinosa A, Di Corato R, Kolosnjaj-Tabi J, Flaud P, Pellegrino T, Wilhelm C (2016) Duality of iron oxide nanoparticles in cancer therapy: amplification of heating efficiency by magnetic hyperthermia and photothermal bimodal treatment. ACS Nano 10(2):2436–2446. https://doi.org/10.1021/acsnano.5b07249

Evertsson M, Kjellman P, Andersson M, Tran TA, In’t Zandt R, Grafstrom G, Toltevall H, Fredrikszon S, Ingvar C, Strand SE, Jansson T (2017) Combined Magnetomotive ultrasound, PET/CT, and MR imaging of (68)Ga-labelled superparamagnetic iron oxide nanoparticles in rat sentinel lymph nodes in vivo. Sci Rep 7(1):4824. https://doi.org/10.1038/s41598-017-04396-z

Fayemi OE, Adekunle AS, Ebenso EE (2017) Electrochemical determination of serotonin in urine samples based on metal oxide nanoparticles/MWCNT on modified Glassy Carbon Electrode. Sens Bio Sens Res 13:17–27. https://doi.org/10.1016/j.sbsr.2017.01.005

Fornara A, Johansson P, Petersson K, Gustaffson S, Qin J, Olsson E, Ilver D, Krozer A, Muhammed M, Johansson C (2008) Tailored magnetic nanoparticles for direct and sensitive detection of biomolecules in biological samples. Nano Lett 8(10):3423–3428. https://doi.org/10.1021/nl8022498

Freeman AC, Platt SR, Holmes S, Kent M, Robinson K, Howerth E, Eagleson J, Bouras A, Kaluozova M, Hadjiyanis CG (2018) Convexion-enhanced delivery of cetuximab conjugated iron-oxide nanoparticles for treatment of spontaneous canine intracranial gliomas. J Neurooncol 137(3):653–663. https://doi.org/10.1007/s10003-016-2764-1

Gao L, Fan K, Yan X (2017) Iron oxide nanomycete: a multifunctional enzyme mimic for biomedical applications. Theranostics 7(13):3207–3227. https://doi.org/10.7150/thno.19738

García RS, Stafford S, YK Gk (2018) recent progress in synthesis and functionalization of multimodal fluorescent-magnetic nanoparticles for biological applications. Appl Sci 8(2):172. https://doi.org/10.3390/app8020172

Gawande MB, Goswami A, Felpin FX, Asefa T, Huang X, Silva R, Zou X, Zboril R, Varma RS (2016) Cu and Cu-based nanoparticles: synthesis and applications in catalysis. Chem Rev 116(6):3722–3811. https://doi.org/10.1021/acs.chemrev.5b00482

Gupta AK, Gupta M (2005) Synthesis and surface engineering of iron oxide nanoparticles for biomedical applications. Biomaterials 26(18):3995–4021. https://doi.org/10.1016/j.biomaterials.2004.10.012

Gupta AK, Naregalkar RR, Vaidya JD, Gupta M (2007) Recent advances on surface engineering of magnetic iron oxide nanoparticles and their biomedical applications. Nanomedicine (Lond) 2(1):23–39. https://doi.org/10.2217/17435889.2.1.23

Gupta JP, Jaiswal M, Agarwal M, Bahadur D (2018) Superparamagnetic iron oxide-reduced graphene oxide nanohybrid—a vehicle for targeted drug delivery and hyperthermia treatment of cancer. J Magn Magn Mater 448:332–338. https://doi.org/10.1016/j.jmmm.2017.05.084

He R, Wang YC, Wang X, Wang Z, Liu G, Zhou W, Wen L, Li Q, Wang X, Chen X, Zeng J, Hou JG (2014) Facile synthesis of pentacle gold-copper alloy nanocrystals and their plasmonic and catalytic properties. Nat Commun 5:4327. https://doi.org/10.1038/ncomms5327

Hongmei Jing PW, Ping Yang X, Ke G, Xia B Chen (2010) Magnetic Fe3O4 nanoparticles and chemotherapeutics agents interact synergistically to induce apoptosis in lymphoma cells. Int J Nanomed 5:999–1004. https://doi.org/10.2147/IJN.S14957

Hongwei Chen JB, Zhang F, Zhang J, Paholaka H, Duxin Sun (2014) Highly crystallized iron oxide nanoparticles as effective and biodegradable mediators for photothermal cancer therapy. J Mater Chem B 2(7):757–765

Hope MD, Hope TA, Zhu C, Faraji F, Haraldsson H, Or dovaz KS, Saloner D (2015) Vascular imaging with ferumoxytol as a contrast agent. AJR Am J Roentgenol 205(3):W366–373. https://doi.org/10.2214/AJR.15.14534

Huang DM, Hsiao JK, Chen YC, Chien LY, Yao M, Chen YK, Ko BS, Hsu SC, Tai LA, Cheng HY, Wang SW, Yang CS, Chen YC (2009) The promotion of human mesenchymal stem cell proliferation by superparamagnetic iron oxide nanoparticles. Biomaterials 30(22):3645–3651. https://doi.org/10.1016/j.biomaterials.2009.03.032

Huber DL (2005) Synthesis, properties, and applications of iron nanoparticles. Small 1(5):482–501. https://doi.org/10.1002/smll.200500006

Huilan Yue GZ, Xiaohang Liu C, Li T, Zhou Y, Tao Y, Kang J, Tang SY, Liu B, Xin Zeng, Gen Zhang (2016) Fe3O4 nanoparticles with Ursolic methyl ester induce apoptosis of multidrug-resistant leukemia KA cell: in vitro evaluation. J Nanosci Nanotechnol (16):7140–7144. https://doi.org/10.1166/jnn.2016.11365

Isa Karimzadeh MA, Taher Doroudi MR, Ganjali, Peir Hossein Kolivand (2017) Superparamagnetic iron Oxide (Fe3O4) nanoparticles coated with PEG/PEI for biomedical applications: a facile and scalable preparation route based on the cathodic electrochemical deposition method. Adv Phys Chem 2017:1–7. https://doi.org/10.1155/2017/9437487

Ismail RA, Sulaaiman GM, Abdulrahman SA, Marzoog TR (2015) Antibacterial activity of magnetic iron oxide nanoparticles synthesized by laser ablation in liquid. Mater Sci Eng C Mater Biol Appl 53:286–297. https://doi.org/10.1016/j.msec.2015.04.047

Jia Y, Zhang H, Yu J, Tong S, Tian N, Wang Z, Wang X, Xu C, Chu X, Lin J, Ding Y, Li G, Sheng F, Hou Y (2017) Monodisperse Au–Fe3C Janus nanoparticles: an attractive multifunctional material for triple-modal imaging-guided tumor photothermal therapy. ACS Nano 11(9):9239–9248. https://doi.org/10.1021/acs.nanolett.7b04461

Kacar C, Erden PE, Pekyaridimci S, Kilic E (2013) An Fe3O4-nanoparticles-based amperometric biosensor for creatine determination. Artif Cells Nanomed Biotechnol 41(1):2–7. https://doi.org/10.3390/app8020172

Kandasamy GSA, Bhati P, Chakrabarty A, Maity D (2018a) Systematic investigations on heating effects of carboxyl-amine functionalized superparamagnetic iron oxide nanoparticles (SPIONs) based ferrofluids for in vitro cancer hyperthermia therapy. J Mol Liq 256:224–237. https://doi.org/10.1016/j.molliq.2018.02.029

Kandasamy GSA, Luthra T, Saini K, Maity D (2018b) Functionalized hydrophobic superparamagnetic iron oxide nanoparticles for magnetic fluid hyperthermia application in liver cancer treatment. ACS Omega 3(4):3991–4005. https://doi.org/10.1021/acsomega.8b00207

Karim MN, Anderson SR, Singh S, Ramanathan R, Bansal V (2017) Nanostructured silver fabric as a free-standing NanoZyme for colorimetric detection of glucose in urine. Biosens Bioelectron 98:109–115. https://doi.org/10.1016/j.bios.2018.03.025

Kievit FM, Zhang M (2011) Surface engineering of iron oxide nanoparticles for targeted cancer therapy. Acc Chem Res 44(10):853–862. https://doi.org/10.1021/ar2000277
Kolosnjaj-Tabi J, Wilhelm C (2017) Magnetic nanoparticles in cancer therapy: how can thermal approaches help? Nanomedicine (Lond) 12(6):573–575. https://doi.org/10.2217/nmn-2017-0014

Larson TA, Joshi PP, Sokolov K (2012) Preventing protein adsorption and macropage uptake of gold nanoparticles via a hydrophobic shield. ACS Nano 6(10):9182–9190. https://doi.org/10.1021/nn3035155

Lee HY, Li Z, Chen K, Hsu AR, Bortot B, Lu C, Cava F, Marin MG, Severini GM, Terreno E, Comes Franchini M (2017) Synthesis of lipophilic core-shell Fe3O4@SiO2@Au nanoparticles and polymeric entrapment into nanocellucles: a novel nanosystem for in vivo active targeting and magnetic resonance-photonacoustic dual imaging. Bioconjug Chem 28(5):1382–1390. https://doi.org/10.1021/acs.bioconjugchem.7b00076

Mónica Carril I, Juan Rodríguez I, Penades GS (2014) Gold-coated iron oxide glyconanoparticles for MRI, CT, and US multimodal imaging. Part Part Syst Charact 31:81–87. https://doi.org/10.1002/ppsc.201300239

Nahrendorf M, Zhang H, Hembrador S, Panizzi P, Nosovik DE, Akaiwa E, Libby P, Swirski FK, Weissleder R (2008) Nanoparticle PET-CT imaging of macrophages in inflammatory atherosclerosis. Circulation 117(3):379–387. https://doi.org/10.1161/CIRCULATIONAHA.107.741181

Nawazehb Solarizadeh MS, Farhood Heydari, Seyyed Salman Seyyed Afghahi (2017) Preparation and physico-biochemical characterization of (Fe, Co, Ni) oxide nanoparticles-decorated PANI-MWCNTs as peroxidase mimetics. New J Chem 41:14049–14052. https://doi.org/10.1039/C7NJ01159G

Nehra P, Chauhan RP, Garg N, Verma K (2018) Antibacterial and antifungal activity of chitosan coated iron oxide nanoparticles. Br J Biomed Sci 75(1):13–18. https://doi.org/10.1080/09674845.2017.1347362

Niu C, Xu Y, An S, Zhang M, Hu Y, Wang L, Peng Q (2017) Near-infrared induced phase-shifted ICG/Fe3O4 loaded PLGA nanoparticles for photothermal tumor ablation. Sci Rep 7(1):5490. https://doi.org/10.1038/s41598-017-06122-1

Nor NM., Lockman Z (2017) Physical and electrochemical properties of iron oxide nanoparticles-modified electrode for amperometric glucose detection. Electrochim Acta 248:160–168. https://doi.org/10.1016/j.electacta.2017.07.097

Patra JK, Ali MS, Oh IG, Baek KH (2017) Proteasome inhibitory, antioxidant, and synergistic antibacterial and antifungal activity of green synthesized magnetic Fe3O4 nanoparticles using the aqueous extract of corn (Zea mays L.) ear leaves. Artif Cells Nanomed Biotechnol 45(2):349–356. https://doi.org/10.3109/21691401.2016.1153484

Pellico J, Ruiz-Cabello J, Fernandez-Barahona I, Gutierrez L, Lechuga-Vieco AV, Enriquez JA, Morales MP, Herranz F (2017) One-step fast synthesis of nanoparticles for MRI: coating chemistry as the key variable determining positive or negative contrast. Langmuir 33(39):10239–10247. https://doi.org/10.1021/acs.langmuir.7b01175

Perlman O, Azhari H (2017) Ultrasonic computed tomography imaging of iron oxide nanoparticles. Phys Med Biol 62(3):825–842. https://doi.org/10.1088/1361-6560/aa51ab

Pirayesh-Islamian J, Hatamian M, Aval NA, Rashidi MR, Mesbah A, Mohammadzadeh M, AsgharJafariabadi M (2017) Targeted superparamagnetic nanoparticles coated with 2-deoxy-D-glucose and doxorubicin more sensitize breast cancer cells to ionizing radiation. Breast 33:97–103. https://doi.org/10.1016/j.breast.2017.03.009

Mazairo A, Bellkaha AFH, Lomas JS, Decorre P, Chevillot-Biraud A, Verbeke P, Wilhelm C, Ammar S, El Hage J-M, Chahine M, Hamadi (2017) Functionallization of iron oxide nanoparticles with HSA protein for thermal therapy. IEEE Trans Magn 53(11). https://doi.org/10.1109/TMAG.2017.2707599

Monaco I, Arena F, Biffi S, Locatelli E, Bortot B, La Cava F, Marinig GM, Severini GM, Terreno E, Comes Franchini M (2017) Synthesis of lipophilic core-shell Fe3O4@SiO2@Au nanoparticles and polymeric entrapment into nanocellucles: a novel nanosystem for in vivo active targeting and magnetic resonance-photonacoustic dual imaging. Bioconjug Chem 28(5):1382–1390. https://doi.org/10.1021/acs.bioconjugchem.7b00076

Lee MS, Su CM, Yeh JC, Wu PR, Tsai TY, Lou SL (2016) Synthesis of composite magnetic nanoparticles Fe3O4@Au with alendronate for oesporosis treatment. Int J Nanomed 11:4583–4594. https://doi.org/10.2147/IJN.S12415

Liang H, Liu B, Yuan Q, Liu J (2016) Magnetic iron oxide nanoparticle seeded growth of nucleotide coordinated polymers. ACS Appl Mater Interfaces 8(24):15615–15622. https://doi.org/10.1021/acsami.6b04038

Lin T, Zhong L, Guo L, Fu C, Chen G (2014a) Seeing diabetes: visual detection of glucose based on the intrinsic peroxidase-like activity of MoS2 nanosheets. Nanoscale 6(20):11856–11862. https://doi.org/10.1039/c4nr03393k

Lin T, Zhong L, Song Z, Guo L, Wu H, Guo Q, Chen Y, Fu F, Chen G (2014b) Visual detection of blood glucose based on peroxidase-like activity of WS2 nanosheets. Biosens Bioelectron 62:302–307. https://doi.org/10.1016/j.bios.2014.07.001

Lin Y, Huang Y, Ren J, Qu X (2014c) Incorporating ATP into biomimetic catalysts for realizing exceptional enzymatic performance over a broad temperature range. Npg Asia Mater 6:e114. https://doi.org/10.1038/am.2014.42

Lin Y, Ren J, Qu X (2014d) Catalytically active nanomaterials: a promising candidate for artificial enzymes. Acc Chem Res 47(4):1097–1105. https://doi.org/10.1021/ar400250z

Lindholm P, Minn H, Leskenin-Kallio S, Bergman J, Ruotsalainen U, Jonnus H (1993) Influence of the blood glucose concentration on FDG uptake in cancer—a PET study. J Nucl Med 34(1):1–6

Ling-feng Min L-IH, Chen Q, Yu Q, Ming-xuan X (2012) Magnetic iron oxide nanoparticles carrying PTEN gene to reverse cisplatin-resistance of A549/CDDP cell lines. J Central South Univ 19:331–339. https://doi.org/10.1007/s11771-012-1009-2

Liu Z, Cai W, He L, Nakayama N, Chen K, Sun X, Chen X, Dai H (2007) In vivo biodistribution and highly efficient tumour targeting of carbon nanotubes in mice. Nat Nanotechnol 2(1):47–52. https://doi.org/10.1038/nnano.2006.170

Liu J, Xu J, Zhou J, Zhang Y, Guo D, Wang Z (2017) Fe3O4-based PLGA nanoparticles as MR contrast agents for the detection of thrombosis. Int J Nanomedicine 12:1115–1126. https://doi.org/10.2147/IJN.S123228

Mahajan UM, Teller S, Sendler M, Palankar R, van den Brandt C, Schweiger T, Kuhn JP, Ribback S, Gloekl G, Evert M, Weitschies W, Hosten N, Dombrowski F, Delcea M, Weiss FU, Lerch MM, Mayerle J (2016) Tumour-specific delivery of siRNA-coupled superparamagnetic iron oxide nanoparticles, targeted against PLK1, stops progression of pancreatic cancer. Gut 65(11):1838–1849. https://doi.org/10.1136/gutjnl-2016-311393

Mahato K, Kumar A, Maurya PK, Chandra P (2018a) Shifting paradigm of cancer diagnoses in clinically relevant samples based on miniaturized electrochemical nanobiosensors and microfluidic devices. Biosens Bioelectron 100:411–428. https://doi.org/10.1016/j.bios.2017.09.003

Mahato K, Maurya PK, Chandra P (2018b) Fundamentals and commercial aspects of nanobiosensors in point-of-care clinical diagnostics. 3 Biotech 8(3):149. https://doi.org/10.1007/s13205-018-1148-8
with near-infrared light. Nat Mater 8(12):935–939. https://doi.org/10.1038/nmat2564
Ye P, Kong Y, Chen X, Li W, Liu D, Xie Y, Zhou Y, Zou H, Chang Z, Dai H, Kong X, Liu P (2017) Fe3O4 nanoparticles and cryoablation enhance ice crystal formation to improve the efficiency of killing breast cancer cells. Oncotarget 8(7):11389–11399. https://doi.org/10.18632/oncotarget.13859
Ye F, Huang Y, Cole AJ, Yang VC (2009) The artificial peroxidase activity of magnetic iron oxide nanoparticles and its application to glucose detection. Biomaterials 30(27):4716–4722. https://doi.org/10.1016/j.biomaterials.2009.05.005
Zhao JDW, Zhang X, Chai H, Huang Y (2018) FeNPs@Co3O4 hollow nanocages hybrids as effective peroxidase mimics for glucose biosensing. Sens Actuators B 263:575–584. https://doi.org/10.1016/j.snb.2018.02.151
Zheng X, Liu Q, Jing C, Li Y, Li D, Luo W, Wen Y, He Y, Huang Q, Long YT, Fan C (2011) Catalytic gold nanoparticles for nanoplasmic detection of DNA hybridization. Angew Chem Int Ed Engl 50(50):11994–11998. https://doi.org/10.1002/anie.201105121
Zheng XC, Ren W, Zhang S, Zhong T, Duan XC, Yin YF, Xu MQ, Hao YL, Li ZT, Li H, Liu M, Li ZY, Zhang X (2018) The theranostic efficiency of tumor-specific, pH-responsive, peptide-modified, liposome-containing paclitaxel and superparamagnetic iron oxide nanoparticles. Int J Nanomed 13:1495–1504. https://doi.org/10.2147/IJN.S157082
Zhou Z, Sun Y, Shen J, Wei J, Yu C, Kong B, Liu W, Yang H, Yang S, Wang W (2014) Iron/iron oxide core/shell nanoparticles for magnetic targeting MRI and near-infrared photothermal therapy. Biomaterials 35(26):7470–7478. https://doi.org/10.1016/j.biomaterials.2014.04.063