Medial patellofemoral ligament is a part of the vastus medialis obliquus and vastus intermedius aponeuroses attaching to the medial epicondyle

Suthasinee Tharnmanularp1 · Akimoto Nimura2* · Masahiro Tsutsumi1,3 · Mio Norose1 · Sachiyuki Tsukada1 · Keiichi Akita1

Received: 12 November 2021 / Accepted: 11 April 2022 / Published online: 6 May 2022
© The Author(s) 2022

Abstract
Purpose This study aimed to investigate the bony surface characteristic of the femoral attachment of the medial patellofemoral ligament (MPFL) and the correlation between the relevant layered structures, including muscular aponeurosis and the joint capsule, which contribute to patellofemoral joint (PFJ) stability.

Methods The morphology of the medial aspect of the medial condyle using micro-computed tomography and analysed cortical bone thickening in 24 knees was observed. For the macroscopic and histological analyses, 21 and 3 knees were allocated, respectively. The Kruskal–Wallis one-way analysis of variance test with Dunn post hoc testing was performed for statistical analysis.

Results At the level of the adductor tubercle, there were no significant differences in cortical bone thickness. At the level of the medial epicondyle (MEC), cortical bone thickness was considerably greater than that in other areas of the medial condyle (mean ± standard deviation, 0.60 ± 0.20 mm; \(p < 0.0001\)). Macroscopic analysis revealed that the deep aponeurosis of the vastus medialis obliquus and the tendinous arch of the vastus intermedius distally formed the composite membrane and adjoined to the joint capsule to firmly attach to MEC, which was located at 41.3 ± 5.7 mm posterior and 14.2 ± 3.1 mm superior to the joint cartilage. Histological analysis showed a composite membrane and adjoining capsule attached to MEC via fibrocartilage.

Conclusion MPFL could be interpreted as part of the deep aponeurosis of the vastus medialis obliquus (VMO) and the tendinous arch of the vastus intermedius, which combined with the joint capsule to attach to MEC. The cortical bone thickening indicated that the tensile stresses were loaded on MEC in aged cadavers. Involvement of VMO and vastus intermedius aponeuroses in restored graft of MPFL could utilise the dynamic stability of surrounding muscles to mimic a native structure.

Keywords Medial patellofemoral ligament · Vastus medialis obliquus · Vastus intermedius · Aponeurosis · Joint capsule · Adductor tubercle · Medial epicondyle · Cortical bone thickness

Abbreviations

| Abbreviation | Description |
|--------------|-------------|
| PFJ          | Patellofemoral joint |
| MPFL         | Medial patellofemoral ligament |
| VMO          | Vastus medialis obliquus |
| micro-CT     | Micro-computed tomography |
| 3D           | Three-dimensional |
| MEC          | Medial epicondyle |
| ICCs         | Intraclass correlation coefficients |

* Akimoto Nimura
nimura.orj@tmd.ac.jp

1 Department of Clinical Anatomy, Graduate School of Medical and Dental Sciences, Tokyo Medical and Dental University, Tokyo, Japan
2 Department of Functional Joint Anatomy, Graduate School of Medical and Dental Sciences, Tokyo Medical and Dental University, 1-5-45 Yushima, Bunkyo-ku, Tokyo 113-8519, Japan
3 Inclusive Medical Science Research Institute, Morinomiya University of Medical Sciences, Osaka, Japan
Introduction

Medial patellofemoral ligament (MPFL) has been commonly reconstructed to treat chronic lateral patellar instability [15, 20, 45]. However, there is currently no consensus on the method of MPFL reconstruction and rehabilitation that best restores natural function. Precise anatomical understanding of the MPFL is essential for managing the patellofemoral joint (PFJ) stability, especially since the femoral attachment sites have been demonstrated at various positions on medial femoral condyle in different studies [1, 45]. Histologically, the arrangements and boundaries of ligaments, tendons, and aponeuroses are vague [35]. Better anatomical understanding of these surrounding structures may help elucidate the mechanisms of the PFJ stability and further clarify the definition of the ligaments [2, 11, 41, 43].

Previously, high stresses transmitted through dense connective tissues, such as tendons, ligaments, and aponeuroses, have been shown to influence the morphology and cortical bone thickness at the attachment site [11, 25, 27, 37, 39, 40]. To date, the morphology of the medial condyle in relation to the tensile stress involve in the PFJ stability has been rarely discussed.

The aim of this study was to investigate the bony surface characteristic of the femoral attachment and the correlation between the relevant layered structures, including the muscular aponeurosis and joint capsule, in reference to the MPFL attachment. Considering the clinical implications, the involvement of surrounding aponeuroses in restored graft of MPFL could utilise the dynamic stability of muscles to mimic the structure of a native knee. It was hypothesised that the medial aspect of the medial condyle had a particular characteristic corresponding to the surrounding fibrous structures, which would contribute to PFJ stability, and after separating the adjoining vastus medialis obliquus (VMO), vastus intermedius aponeurosis, and joint capsule, the remaining part of these fibrous structures was assumed to be the MPFL.

Materials and methods

Cadaveric specimen preparations and micro-computed (micro-CT) tomography imaging

The ethical approvals was issued by the institutional review board of Tokyo Medical and Dental University (M2018-243-01). Twenty-five knees (11 pairs and 3 halves, including 13 right and 12 left knees) from 14 cadavers (six men, eight women; mean age and standard deviation, 84.6 ± 10.4 years) were obtained for this study. No specimens with a severe deformity of the knee joint or past histories of knee surgery were included. All the cadavers were donated to the Department of Anatomy of the Tokyo Medical and Dental University.

All specimens were fixed in 8% formalin and preserved in 30% ethanol. The medial regions of the knee were harvested by cutting at the distal one-third of the femur, tibial tuberosity, and midline of the sagittal plane using a diamond band pathology saw (EXAKT 312; EXKAKT Advanced Technologies GmbH, Norderstedt, Germany). After removing the skin and subcutaneous soft tissues, three-dimensional (3D) images of all medial halves of the knee using micro-CT (inspeXio SMX-100CT; Shimadzu Corp., Kyoto, Japan) with 200-µm resolution and ImageJ (version 1.52; National Institutes of Health, Bethesda, MD, USA) were obtained. One knee with a varus deformity on the 3D image was excluded. To confirm the correspondence between the 3D-CT image and actual bony surface without dissection artefacts, the soft tissues were removed in three specimens using an 8% sodium hydroxide solution (Wako Pure Chemical Industries, Osaka, Japan). In the remaining 21 specimens, 18 and 3 knees were randomly allocated to macroscopic and histological analyses, respectively (Fig. 1).

Cortical bone thickness analysis of the medial condyle of the femur

To visualise the distribution of cortical bone thickening on the medial condyle of the femur, 8-bit images of 24
specimens obtained as described were transferred to ImageJ open-source image processing software (National Institute of Health, Bethesda, MD). The BoneJ plugin, an ImageJ extension for bone image analysis and published image processing algorithms, was used to define the thickness at a specific point by measuring the diameter of the largest sphere that fit within the structure of interest [6, 11, 16, 40]. The measurement was accurate for two-decimal places [10, 25]. The cortical bone thickness of the medial condyle was mapped in 3D images, in which brighter colours represented thicker points of the cortical bone.

To quantify the cortical bone thickness of the medial condyle, axial images at the middle levels of the adductor tubercle and medial epicondyle (MEC) were utilised. The locations of the measurements were divided into equal rectangles for the adductor tubercle (2.0  × 6.0 mm) and MEC (4.0  × 18.0 mm). The pilot trial was carried out to confirm that the rectangle fits the morphology of the cortical bone surface without overlapping boundaries in each measuring area. The rectangles were set parallel to the bony surfaces. The average cortical bone thickness of each rectangle was measured. The measurement was repeated twice in 24 knees randomly on different days using the same method. To determine the test–retest reliability, 48 measurements were compared between two examination days. All ICC scores were ≥ 0.92 (range 0.92–0.99).

**Macroscopic observation of the fibrous structures attaching to the medial epicondyle of the femur**

After removing the skin and subcutaneous tissue, the sartorius, gracilis, and semitendinosus muscles were identified and reflected anteriorly. Next, the VMO was identified on the medial aspect of the knee. To identify the deep aponeurosis of the VMO, the VMO muscle portion was first removed. Then, the deep aponeurosis of the VMO was reflected anteriorly to reveal the vastus intermedius and its tendinous arch. The tendinous structures and joint capsule were detached en bloc from the medial condyle to clarify the relationships between the tendinous structures, joint capsule, and femoral attachment. Additionally, the location of the attachment on the femur’s medial aspect was measured using a non-digital Vernier calliper which allows measurement to one decimal. The measurements were taken twice in 18 knees on separate days using the same procedure. To validate the accuracy, 36 measurements were compared between two assessment days. All ICC scores were ≥ 0.98 (range 0.98–0.99).

**Histological analysis of the medial condyle of the femur**

Three knees were randomly selected for histological analysis. Specimens were embedded in agar solution (22 g/L) and frozen at – 80 °C. Subsequently, specimens were cut horizontally into 5-mm-thick blocks using a band saw (WN-25-3; Nakajima Seisakusho, Osaka, Japan). Two blocks of axial slices were selected at the adductor tubercle and MEC levels. A 3D-CT image was used to validate the level. En bloc specimens were decalcified for 1 week in Plank-Rychlo solution (AlCl₃; 6H₂O, 126.7 g/L; HCl, 85.0 mL/L; HCOOH, 50.0 mL/L) [33, 42, 43]. After decalcification, the blocks were dehydrated with a graded ethanol series, embedded in paraffin, and serially sectioned (thickness, 5 µm). Finally, staining was performed using the Manson trichrome staining protocol.

**Statistical analysis**

The Kruskal–Wallis one-way analysis of variance test with Dunn post hoc testing was performed to compare the cortical bone thicknesses at measured locations in the axial slices at the adductor tubercle and MEC levels. Statistical significance was set at p values of < 0.05. To evaluate the test–retest reliability, a single observer randomly measured the specimens twice on different days in the same approach. The intraclass correlation coefficients (ICCs) were determined for each parameter. A score of > 0.75 was considered an excellent agreement. Data are presented as mean and standard deviation. Statistical analyses were performed using PASW Statistics 18 for Windows (SPSS Inc., Chicago, IL, USA).

To calculate the sample size for the cortical bone thickness analysis, the estimated cortical bone thickness from a previous relevant study that investigated the tibia and fibula was utilised [41]. Using the one-way analysis of variance, a 2-sided type I error of 0.05, 90% power, a minimum sample of 18 per area was required (nQuery Advisor® Version 6.01; Statistical Solutions Ltd., Saugus, MA, USA). More samples were analysed to spare the number of specimens in case dropout during the study. The total number of investigated specimens in this study was 24.

**Results**

**Bone morphological features of the medial condyle of the femur using micro-CT**

Distal to the adductor tubercle, which was small and rough, the MEC was shaped as a wide shelving prominence (Fig. 2A). The proximal part of the MEC was continuous with the distal margin of the adductor tubercle. The anterior edge of the MEC was easily identifiable, whereas the posterior and inferior edges were unclear. These bony morphologies could be additionally confirmed as actual bone using chemical debridement (Fig. 2B).
The cortical bone thickness measurement revealed that thickening was evident on the MEC, compared with the other areas of the medial condyle (Fig. 3). Data at the level of the adductor tubercle and MEC are shown in Table 1.

**Layered relationships between the fibrous structures attaching the medial epicondyle of the femur**

The deep aponeurosis of the VMO was observed to transition into the VMO tendon, which attached to the superomedial border of the patella (Fig. 4A, B). The tendinous arch of the vastus intermedius was exposed posteriorly to the VMO's deep aponeurosis, which distally merged into the tendinous arch of the vastus intermedius to form the composite membrane (Fig. 4C). The joint capsule was underlaid deep into the composite membrane, which was distally intermingled with the joint capsule and firmly attached to the MEC (Fig. 4D).

Viewing from the intra-articular side, the deep part of the composite membrane was observed to distally merge with the joint capsule and firmly attach to the MEC (Fig. 5). The firmly attached area of the composite membrane and joint capsule are summarised in Table 2.

---

**Fig. 2** Morphology of the adductor tubercle and medial epicondyle. The medial aspect of the medial condyle of the right femur. The medial epicondyle (MEC; white circle) is located distal to the adductor tubercle (asterisk). The anterior margin of the MEC (dotted line) was remarkable in comparison with the posterior and inferior margins. A The medial condyle was examined using micro-computed tomography (micro-CT). B In the same specimen as A, soft tissues were chemically removed to assess correlations with the micro-CT image. Ant, anterior; Prox, proximal

**Fig. 3** Evaluation of cortical bone thickening in the medial condyle of the femur. The cortical thickening maps on the right medial condyle were visualised after processing the micro-computed tomography (micro-CT) images. The thicker the cortical bone of the point, the brighter the colour of the point. A Three-dimensional image of the medial condyle surface. Levels of axial slices are shown as white dotted lines. B Axial image at the middle level of the adductor tubercle (asterisk). The mean cortical bone thickness was measured in each rectangle from the anterior to posterior part of the adductor tubercle (from AT1 to AT3). C Axial image at the level of the apex of the medial epicondyle (white circle). The mean cortical bone thickness was measured in each rectangle from the anterior to posterior part of the medial epicondyle (from ME1 to ME3). The cortical thickness distribution (mm) is shown as the spectrum from black to marine blue, violet, red, orange, yellow, and white. Ant, anterior; Med, medial; Prox, proximal
Histological analyses of the fibrous structures on the medial condyle of the femur

At the level of the adductor tubercle, the deep aponeurosis of the VMO was identified as a remarkable fibrous layer accompanied by a robust muscular portion (Fig. 6A, B). The joint capsule was identified as the innermost layer connecting the joint cavity. The tendinous arch of the vastus intermedius was observed as a thin fibrous layer interposed between the deep aponeurosis of the VMO and the joint capsule.

At the MEC level, the composite membrane adjoined the joint capsule and was attached to the MEC via fibrocartilage (Fig. 6A, C).

Discussion

The most important findings of the present study were that the cortical bone thickness of the MEC was significantly greater than that of the other areas on the medial condyle, and the deep aponeurosis of the VMO and the tendinous arch of the vastus intermedius formed the composite membrane to firmly attach to the MEC via fibrocartilage.

As previous reports, the bone is a highly adaptive structure under a mechanical stress load. Since the bone is thicker in areas that are subject to high stress, the distribution of cortical bone thickening could represent areas of high tensile stress, allowing the definition of functional attachment for fibrous structures [10, 25, 40]. The present study revealed that cortical bone thickening was limited in the MEC. This finding suggests that the tensile stress from the stabilising structures against lateral patellar translation is focussed on the MEC, regardless of the structure attached on it.

The MPFL is considered as a primary restrictor to maintain PFJ stability, whereas the medial patellotibial ligament (MPTL) and medial patellomeniscal ligament (MPML) are regarded as secondary stabilisers [7, 9, 17]. The MPFL has been described as a fan-like structure extending from the medial part of the femoral condyle to the superomedial edge of the patella [3, 19, 32, 45], associates with the VMO’s undersurface [13, 19, 26] and connects with the aponeurosis of the vastus intermedius [3, 23]. However, the layered relationship between the MPFL and surrounding structures, including the aponeurosis and

| Location of Measurement | Mean ± SD (mm) |
|-------------------------|---------------|
| Adductor tubercle level  |               |
| Anterior most (AT1)     | 0.47 ± 0.10   |
| Anterior to adductor tubercle (AT2) | 0.49 ± 0.11 |
| Anterior aspect of adductor tubercle (AT3) | 0.43 ± 0.09 |
| Posterior aspect of adductor tubercle (AT4) | 0.45 ± 0.09 |
| Posterior to adductor tubercle (AT5) | 0.46 ± 0.12 |
| Medial epicondyle level |               |
| Anterior to medial epicondyle (ME1) | 0.36 ± 0.08 |
| Medial epicondyle (ME2) | 0.60 ± 0.20*  |
| Posterior to medial epicondyle (ME3) | 0.36 ± 0.13 |

The area of the measurements is demonstrated in Fig. 2

SD standard deviation, AT adductor tubercle, ME medial epicondyle

*Highly statistically significant difference compared to the other areas (p value < 0.0001; the Kruskal–Wallis one-way analysis of variance test with Dunn post hoc test was conducted)

Fig. 4 Layered relationships between the fibrous structures attached to the medial epicondyle. A The medial aspect of the right femur. The superficial fascia was removed, and the vastus medialis oblique (VMO) muscle is shown. B After removing the muscular portion of the VMO, the sartorius (Sa), gracilis (Gr), and semitendinosus (St) muscles are reflected to the anterior. The deep aponeurosis of the VMO (VMO-da) and posterior part of the composite membrane are exposed. C The VMO-da is reflected anteriorly. The tendinous arch of the vastus intermedius (VI) posterodistally continues to the composite membrane. The dashed line indicates the posterior margin of the tendinous arch of the VI. D The VI is reflected anteriorly. The composite membrane comprising the VMO-da and tendinous arch of the VI attaches to the MEC (black circle). AM, adductor magnus; Ga-m, medial head of the gastrocnemius; RF, rectus femoris; SM, semimembranosus; TCL, tibial collateral ligament; Ant, anterior; Prox, proximal
The deep aponeurosis of the vastus medialis obliquus (VMO-da), tendinous arch of the vastus intermedius (VI), and joint capsule, are detached en bloc from the medial condyle of the femur and posteriorly reflected. Black solid lines indicate the proximal edge of the joint cartilage and corresponding part of the joint capsule. B The composite membrane is detached more posteriorly than A, and the adductor tubercle (asterisk) and medial epicondyle (MEC; black circle) are shown. C The composite membrane was detached more posteriorly than B to expose the firmly attached area to the MEC. Black dotted lines indicate the anterior margin of the firmly attached area of the composite membrane and the corresponding part of the membrane. The location of the firmly attached area on the MEC was measured from the medial (X) and proximal (Y) edges of the joint cartilage. D Distally reflecting the joint capsule, the connection between the joint capsule and tendinous arch of the VI is shown. AM, adductor magnus; Ga-m, medial head of the gastrocnemius; SM, semimembranosus; VI, vastus intermedius; Ant, anterior; Prox, proximal

Table 2 The firmly attached area of the composite membrane and joint capsule on the medial aspect of the medial femoral condyle

| Location                        | Mean ± SD (mm) |
|---------------------------------|----------------|
| Posterior to the edge of the joint cartilage (X) | 41.3 ± 5.6     |
| Superior to the edge of the joint cartilage (Y)   | 14.2 ± 3.1     |

The area of the measurements is demonstrated in Fig. 5C

SD standard deviation
restrain lateral translation of the patellar [28] rather than the independent static cord as assumed from the MPFL.

Recent studies have reported the MPFL’s femoral attachment [14, 30, 31, 46] at various sites, including at the adductor tubercle [24, 44], MEC [3, 5, 23], a point between the adductor tubercle and MEC [19, 29] and the gastrocnemius tubercle [1]. In short, the location of the MPFL’s attachment to the medial condyle remains inconclusive. Based on the results obtained in the present study, the previous inconsistency regarding MPFL femoral attachments could be explained as follows: although the MPFL could be part of the composite membrane, comprising the VMO and vastus intermedius aponeurosis, authors of previous anatomical studies may have assumed the MPFL to be a cord-like structure, artificially separate from the composite membrane, and thus defined the attachment locations differently. The actual composite membrane had a broader attachment to the MEC than the single point assumed by the cord-like MPFL model. In the current study, cortical bone thickening and fibrocartilaginous histology could validate the tensile stress on the MEC transferred by the composite membrane and joint capsule.

This study has several limitations. First, the sample size calculation for the cortical bone thickness analysis might be not be accurate, since previous data of the tibia and fibula and the one-way analysis of variance function were substituted. Second, the number of specimens used for the histological analysis was limited. Third, only the cadavers of older adults were used; therefore, the age was not matched with that of the patients with PFJ instability. Lastly, other bony morphologies were subject to the tensile stress in the relevant area, such as the gastrocnemius tubercle. Further studies are warranted to fully cover the thickness of the cortical bone on the medial side of the knee in relation to the soft tissue attachments. Consequently, we hope to lay the groundwork for subsequent anatomical and biomechanical studies with younger age population, or imaging of clinical cases of the medial part of the femoral condyle in the future.

This study emphasises certain clinical implications of the MPFL. First, considering the closely relationship between MPFL and VMO [28], the superior fibre of the MPFL graft meshed together with the VMO has been recommended during MPFL reconstruction [2, 12]. Based on anatomical findings, both the VMO and vastus intermedius were recommended to be involved in MPFL graft to utilise the dynamic stability of surrounding muscles to mimic the structure of a native knee. Second, since the VMO was thought to medially pull the patella through the MPFL by muscle contraction [18, 24], quadriceps strengthening has been the focus of conservative management strategies for PFJ stability [4, 8, 21, 34, 38]. The structural evidence for the effectiveness of quadriceps strengthening management could be validated.
in the present study. Third, femoral attachment malposition is a critical challenge when performing MPFL [18, 22, 24, 36]. The fact that the MEC corresponded to remarkable cortical bone thickening via fibrocartilaginous attachment of the composite membrane might support in determining the proper location of femoral tunnel fixation.

Conclusion

The deep aponeurosis of the VMO and tendinous arch of the vastus intermedius distally intermingled to form a composite membrane, adjoining the joint capsule to attach to the MEC, which indicates that the MPFL was no more than a part of the adjacent VMO and vastus intermedius aponeurosis. The cortical bone thickening indicated that the tensile stresses were loaded on the MEC in aged cadavers. Involvement of VMO and vastus intermedius aponeuroses in restored graft of MPFL could utilise the dynamic stability of surrounding muscles to mimic a native structure.

Author contributions TS: experimental work, manuscript review. AN: project planning, management of experimental work, manuscript editing. MT: experimental work, manuscript review. MN: experimental work. ST: statistical analysis, manuscript review. KA: grant writing, management of experimental work, manuscript editing.

Declarations

Conflict of interest The authors declare no conflicts of interest.

Funding The present study received financial support from the JA Kyo-sai Research Institute (Agricultural Cooperative Insurance Research Institute). The funding source did not have any role in the study design, data collection, data analysis, interpretation of data, writing of the article, or in the decision to submit the article for publication.

Ethical approval The Medical Research Ethics Committee of Tokyo Medical and Dental University (M2018-243-01).

Informed consent All the cadavers used in this study were donated to Tokyo Medical and Dental University. Before death, all the donors voluntarily expressed their desire to donate their body for anatomical education and study. This system is established in Act on Body Donation for Medical and Dental Education in Japan. Our study completely complied with the law.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article’s Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article’s Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/.

References

1. Aframian A, Smith TO, Tennent TD, Cobb JP, Hing CB (2017) Origin and insertion of the medial patellofemoral ligament: a systematic review of anatomy. Knee Surg Sports Traumatol Arthrosco 25(12):3755–3772
2. Ahmad CS, Brown GD, Shubin Stein BE (2009) The docking technique for medial patellofemoral ligament reconstruction: surgical technique and clinical outcome. Am J Sports Med 37(10):2021–2027
3. Aragao JA, Reis FP, de Vasconcelos DP, Feitosa VL, Nunes MA (2008) Metric measurements and attachment levels of the medial patellofemoral ligament: an anatomical study in cadavers. Clinics (Sao Paulo) 63(4):541–544
4. Chatterji R, White AE, Hadley CJ, Cohen SB, Freedman KB, Dodson CC (2020) Return-to-play guidelines after patellar instability surgery requiring bony realignment: a systematic review. Orthop J Sports Med 8(12):2325967120966134. https://doi.org/10.1177/2325967120966134
5. Dall’Oca C, Elena N, Lunardelli E, Ulgelmo M, Magnan B (2020) MPFL reconstruction: indications and results. Acta Biomed 91(4-s):128–135
6. Doube M, Klosowski MM, Arganda-Carreras I, Cordelières FP, Dougherty RP, Jackson JS et al (2010) BoneJ: free and extensible bone image analysis in ImageJ. Bone 47(6):1067–1079
7. Felli L, Alessio-Mazzola S, Lovoiso S, Capello AG, Formica M, Maffulli N (2021) Anatomy and biomechanics of the medial patello-femoral ligament: a systematic review. Surgeon 19(5):e168–e174
8. Forde C, Haddad M, Hirani SP, Keene DJ (2021) Is an individually tailored programme of intense leg resistance and dynamic exercise acceptable to adults with an acute lateral patellar dislocation? A feasibility study. Pilot Feasibility Stud 7(1):1–13
9. Hinckel BB, Gobbi RG, Demange MK, Pereira CAM, Pécora JR, Natalino RJM et al (2017) Medial patellofemoral ligament, medial patellotibial ligament, and medial patellomeniscal ligament: anatomic, histologic, radiographic, and biomechanical study. Arthroscopy 33(10):1862–1873
10. Horuchi S, Nimura A, Tsutsumi M, Suzuki S, Fujita K, Nozaki T et al (2020) Anatomical relationship between the morphology of the styloid process of the ulna and the attachment of the radioulnar ligaments. J Anat 237(6):1032–1039
11. Hoshika S, Nimura A, Yamaguchi R, Nasu H, Yamaguchi K, Sugaya H et al (2019) Medial elbow anatomy: a paradigm shift for UCL injury prevention and management. Clin Anat 32(3):379–389
12. Huber C, Zhang Q, Taylor WR, Amis AA, Smith C, Hosseini Nasab SH (2020) Properties and function of the medial patellofemoral ligament: a systematic review. Am J Sports Med 48(3):754–766
13. Joseph SM, Fulkerson JP (2019) Medial quadriceps tendon femoral ligament reconstruction technique and surgical anatomy. Arthrosc Tech 8(1):e57–e64
14. Kang HJ, Wang F, Chen BC, Su YL, Zhang ZC, Yan CB (2010) Functional bundles of the medial patellofemoral ligament. Knee Surg Sports Traumatol Arthrosco 18(11):1511–1516
15. Kay J, Memon M, Ayeni OR, Peterson D (2021) Medial patellofemoral ligament reconstruction techniques and outcomes: a scoping review. Curr Rev Musculoskelet Med 14(6):321–327
16. Kleinman WB (2007) Stability of the distal radioulna joint: biomechanics, pathophysiology, physical diagnosis, and restoration
