Optogenetically Induced Seizure and the Longitudinal Hippocampal Network Dynamics

Shin-ichiro Osawa1,8, Masaki Iwasaki1,8, Ryosuke Hosaka2, Yoshiya Matsuzaka3,5,8, Hiroshi Tomita4, Toru Ishizuka5,8, Eiko Sugano4, Eiichi Okumura6, Hiromu Yawo5,7,8, Nobukazu Nakasato6, Teiji Tominaga1, Hajime Mushiake3,8

1 Department of Neurosurgery, Tohoku University Graduate School of Medicine, Sendai, Japan, 2 Department of Applied Mathematics, Fukuoka University, Fukuoka, Japan, 3 Department of Physiology, Tohoku University Graduate School of Medicine, Sendai, Japan, 4 Department of Chemistry and Bioengineering, Faculty of Engineering, Graduate School of Science and Engineering, Iwate University, Morioka, Japan, 5 Department of Developmental Biology and Neuroscience, Tohoku University Graduate School of Life Sciences, Sendai, Japan, 6 Department of Epileptology, Tohoku University Graduate School of Medicine, Sendai, Japan, 7 Center for Neuroscience, Tohoku University Graduate School of Medicine, Sendai, Japan, 8 Core Research of Evolutional Science & Technology (CREST), Japan Science and Technology Agency (JST), Tokyo, Japan

Abstract

Epileptic seizure is a paroxysmal and self-limited phenomenon characterized by abnormal hypersynchrony of a large population of neurons. However, our current understanding of seizure dynamics is still limited. Here we propose a novel in vivo model of seizure-like afterdischarges using optogenetics, and report on investigation of directional network dynamics during seizure along the septo-temporal (ST) axis of hippocampus. Repetitive pulse photostimulation was applied to the rodent hippocampus, in which channelrhodopsin-2 (ChR2) was expressed, under simultaneous recording of local field potentials (LFPs). Seizure-like afterdischarges were successfully induced after the stimulation in both W-TChR2V4 transgenic (ChR2V-TG) rats and in wild type rats transfected with adeno-associated virus (AAV) vectors carrying ChR2. Pulse frequency at 10 and 20 Hz, and a 0.05 duty ratio were optimal for afterdischarge induction. Immunohistochemical c-Fos staining after a single induced afterdischarge confirmed neuronal activation of the entire hippocampus. LFPs were recorded during seizure-like afterdischarges with a multi-contact array electrode inserted along the ST axis of hippocampus. Granger causality analysis of the LFPs showed a bidirectional but asymmetric increase in signal flow along the ST direction. State space presentation of the causality and coherence revealed three discrete states of the seizure-like afterdischarge phenomenon: 1) resting state; 2) afterdischarge initiation with moderate coherence and dominant septal-to-temporal causality; and 3) afterdischarge termination with increased coherence and dominant temporal-to-septal causality. A novel in vivo model of seizure-like afterdischarge was developed using optogenetics, which was advantageous in its reproducibility and artifact-free electrophysiological observations. Our results provide additional evidence for the potential role of hippocampal septo-temporal interactions in seizure dynamics in vivo. Bidirectional networks work hierarchically along the ST hippocampus in the genesis and termination of epileptic seizures.

Introduction

Epileptic seizure is a paroxysmal and self-limited phenomenon characterized by abnormal hypersynchrony of a large population of neurons [1–3]. Focal seizures, or seizures generated in a certain region of the brain, are usually initiated in the presence of pathological causes and propagated to distant normal cortex. The hippocampus and surrounding limbic structures are the sites most prone to focal epileptic seizures, especially those resistant to medications [4,5]. However, our current understanding of seizure genesis (i.e., the mechanism that initiates epileptic seizures in complex neuronal networks) is still limited [6–8].

Electrical stimulation of the brain has long been used to induce epileptogenesis and epileptic seizures. Electrical kindling, the classic model of epileptogenesis, usually takes weeks to induce spontaneous seizures with less than 70% reproducibility [6,9]. Trains of high-frequency electrical stimulations induce seizure-like patterns as “afterdischarges”. However, a pattern of the induced activity can be substantially different from spontaneous seizures in humans [7,10–14]. Although this is a convenient model of epileptic seizures, the electrical stimulation generates large artifacts which interfere with neuronal activity recording in animal models, thus making it difficult to study the underlying physiological mechanism of the onset, propagation and cessation of seizure in vivo. Increasing the arsenal of seizure models is thus required to better pursue for the electrophysiological mechanisms underlying ictogenesis.
afterdischarges in the hippocampus and induction of seizure-like activity during and after the stimulation (Figure 1C). The diffuse and strong expression of Venus protein was confirmed 4–6 weeks later. Repetitive pulse photostimulation was applied to the hippocampus of wild-type Wistar rats transfected with the rAAV-Chr2-Venus vector (n = 3 rats). The AAV carrying a transgene encoding a Chr2V fusion protein driven by the hybrid cytomegalovirus enhancer/chicken beta-actin promoter was injected into the dentate hilus of the septal hippocampus in normal rats. The viral injection was targeted to 1 mm deeper than the site of stimulation, so that the tissue with Chr2 expression was exposed to photostimulus. Intense Chr2V expression in hippocampal neurons was confirmed 4–6 weeks later. Repetitive pulse photostimulation with combinations of parameters of frequency (5, 10, 20 Hz) and duty ratio (0.05, 0.1, 0.2) were delivered under simultaneous LFP recording using a hybrid electrode. Optical intensity and stimulus duration were fixed at 19–22 mW at the tip of optic fiber and at 20 seconds, respectively. Since the amount of Chr2 expression after viral transfection was expected smaller than in transgenic animals, longer stimulation duration was attempted. Next, afterdischarge thresholds to electrical pulse stimulation were compared between Chr2V-TG rats and wild-type Wistar rats (n = 5, each). A high-impedance (1–2 M ohm) monopolar electrode coupled with a bipolar stainless steel electrode was used (PlasticsOne, Roanoke, VA, USA). The afterdischarge threshold, a minimum current intensity that could induce afterdischarges, was measured in the septal hippocampal region. Bipolar electrical stimulation was applied with a constant current electric stimulator (SEN-3301, SS-102J, Nihon Kohden, Tokyo, Japan). Monophasic square pulses with a pulse duration of 1.0 ms were delivered at a frequency of 60 Hz for 1.0 s under the monitoring LFPs with the same settings as described above. The afterdischarge threshold was determined by delivering a series of graded intensities, which started at 50 μA and increased by 30% increments every 30 min until afterdischarge was triggered. We also examined whether afterdischarge induction occurred in the hippocampus of wild-type Wistar rats and in the extra-hippocampal regions of Chr2V-TG rats. For wild-type rats (n = 5), repetitive pulse photostimulation was applied to the septal hippocampus. For Chr2V-TG rats (n = 4), repetitive pulse photostimulation was applied to the septal hippocampus, amygdala, anterior thalamus, and sensori-motor cortices under simultaneous LFP monitoring, similarly as performed in the hippocampus. Stimulation parameters were set at 10 Hz with a duty ratio of 0.05, the optimal parameters for afterdischarge induction in the hippocampus. Optical intensity and stimulus duration were fixed at 19–22 mW at the tip of optic fiber and at 10 seconds, respectively. Photostimulation was repeated 10 times in one location with minimum 5-minute interval, so that the chance of afterdischarge induction was calculated.

Preparation of AAV vector carrying the Chr2 gene construct

The N-terminal fragment (residues 1–315) of Chr2 (GenBank accession no. AF461397) was fused to a fluorescent protein, Venus, in frame at the end of the Chr2V-coding fragment (Chr2V). The Chr2V gene was introduced into the EcoRI and HindIII sites of the 6P1 plasmid. The synapsin promoter was exchanged for a hybrid cytomegalovirus enhancer/chicken...
beta-actin promoter, and AAV-ChR2V was constructed. The pAAV-RC and p-Helper plasmids were obtained from Stratagene (La Jolla, CA, USA). High titer (1–10$^{12}$ particles/mL) rAAV vectors (rAAV-ChR2V) were purified using the method of Auricchio et al [24].

Stereotactic surgery (placement of cannula, optic fiber and electrodes, and injection of viral vector)

Animals were anesthetized with ketamine and xylazine (80 mg and 8 mg/kg, i.p.). Lack of responsiveness was checked by toe pinch every 15 min. Rectal temperature was monitored and maintained at 37.0°C. After a midline scalp incision, burr holes were drilled in the skull over the hippocampal formation and/or sensory-motor cortex. The dura was carefully removed, and optic fiber and/or electrodes were lowered at the coordinates defined in each experiment. A stainless-steel screw was driven into the bone above the contralateral cerebellum and served as ground and recording reference. The coordinates and depth of optic fiber-electrode insertion was determined relative to bregma as (anterior-posterior, AP, -3.6 mm; medial-lateral, ML, -2.5 mm; dorsal-ventral, DV, -2.35 mm), (AP, -5.4 mm; ML, 5.0 mm; DV, -7.0 mm), (AP, -1.8 mm; ML, 1.5 mm; DV, -4.0 mm), (AP, -3.0 mm; ML, 4.5 mm; DV, -7.5 mm) and (AP, 2.0 mm; ML, 3.0 mm; DV, -1.0 mm), respectively for the septal hippocampal formation, temporal hippocampal formation, anterior thalamus, amygdala, and sensorimotor cortex. The coordinates for viral vector injection was AP, -3.6 mm, ML, 2.5 mm, DV, -3.5 mm. The location of fiber/electrode was confirmed histologically. AAV vector infusion was performed using a micro-infusion method as described previously [25].

Photostimulation and electrophysiological recordings

Simultaneous photostimulation and electrical recording were accomplished by using a hybrid optical fiber with electrode (custom-made). A platinum lead and optic fiber (80-μm diameter) was accommodated in an electrically-isolated cannula with a 260-μm diameter. The fiber-optic cable was attached to a 451 nm diode pumped laser (Optohub, Inc., Saitama, Japan), which emitted 1.2–25.0 mW of light at the tip of the fiber. Stimulation was controlled by Powerlab (AD instrument, Inc., Lexington, Australia). Electrophysiological signals were amplified and band-pass-filtered (1000-fold, band-pass 0.07 and 10 kHz) and digitized at 10 kHz by a Multichannel Acquisition Processor (Plexon, Inc., Dallas, TX, USA). Electromyography of the brachial muscles was also simultaneously recorded in a part of experiment. Location of optic fiber/electrode was verified histologically in hematoxylin-eosin stained sections.

c-Fos expression after induced seizure-like afterdischarges

Next, we investigated the brain regions activated by the induced seizure-like afterdischarges. The septal hippocampus of W-TChR2V4 transgenic (ChR2V-TG) rat hippocampus. (A) Schematic drawing of the DNA fragment inserted at the site of the modified mouse Thy-1.2 expression cassette. (B) ChR2V-TG rat hippocampal organization showed that ChR2V fluorescence (green) was dense in all layers except the cell layer marked with DAPI nuclear stain (blue). (C) Schematic drawing of photostimulation to the septal hippocampus of rat brain. (D) Repetitive pulse photostimulation is schematically presented. The duty ratio was calculated as the proportion of the pulse width to the inter-pulse interval.

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Ox22V-TG rats was photostimulated once, and the brain was removed 1 hour later. Two different parameters were used, one for afterdischarge induction (n = 9 rats) and the other for no afterdischarge induction (control, n = 6 rats). Stimulus parameters were 20 mW, 10 Hz, 10 ms pulse width (duty ratio 0.1), and 10 s duration for the former and 20 mW, 0.5 Hz, 10 ms pulse width, 200 s duration for the latter. The 0.5 Hz stimulation was very much below the threshold for afterdischarge induction according to our results. Note that the total durations of photo-pulses were same between two conditions. In the control case, additional pulse photostimulation (20 mW, 10 Hz, 10 ms pulse width, 10 s duration) was performed to induce afterdischarges immediately before brain removal to confirm that the stimulation was appropriately applied to the hippocampus. This control stimulation was not expected to affect c-Fos signals due to its delayed expression profile. c-Fos expression, a surrogate marker of neuronal excitation, was analyzed by immunohistochemical staining.

Rats were deeply anesthetized with a lethal dose of pentobarbital (80 mg per kilogram of body weight, i.p.) and transcardially perfused, first with phosphate buffered saline (PBS) and then with 4% paraformaldehyde. Following perfusion, brains were immersed in 4% paraformaldehyde for 24 h, soaked for 2-3 days in 100% alcohol, cleared in xylene, and embedded in paraffin. Serial coronal brain sections (5 μm) were sectioned on a microtome and labeled with a rabbit polyclonal anti-c-Fos antibody (1:1,000; Santa Cruz, Inc., Santa Cruz, CA, USA), which was detected by the fluorescent secondary Alexa 568 goat anti-rabbit antibody (1:200; Invitrogen, Carlsbad, CA, USA). Sections were then mounted and coverslipped using VECTASHIELD with DAPI (Vector Laboratories, Inc., Burlingame, CA, USA). Gene-expression efficacy was quantified by counting the number of c-Fos positive cells divided by the number of DAPI-positive cells under a microscope (BZ-9000, Keyence, Inc., Osaka, Japan).

The proportion of c-Fos positive cells to total cells (% c-Fos positive cell) was counted in the granule cell layer of the dentate gyrus (DG) and in the pyramidal cell layer of CA3 and CA1 on the septal and temporal sides of the stimulated hippocampal formation. Cell counting was performed on a coronal section made for the septal and temporal hippocampus. The section was chosen by reference to the Watson-Paxinos’s rat brain atlas; AP – 3.6 mm for the septal hippocampus and AP – 5.4 mm for the temporal hippocampus [26]. The former was made adjacent to the optic fiber insertion. The latter included the appearance of the ventral hippocampus. One section was analyzed per animal, each for the septal and temporal hippocampus. The ventral aspect was used for counting in the temporal hippocampus. The counting was performed offline on the images fused from the epifluorescence. Images were reviewed and scored at 200-fold magnification on two different fields of view, each for DG, CA3 and CA1 region. At least 200 granule cells and/or pyramidal cells were counted by two independent observers (SO, MI) and averaged.

Spatio-temporal dynamics of seizure-genesis along longitudinal hippocampal axis

To investigate the spatio-temporal dynamics of seizure-genesis, we performed multisite LFP recording during seizure-like afterdischarge induction. For this experiment, 10 Hz pulse stimulation was delivered for 30 seconds at a 10 ms pulse width (duty ratio 0.1) and a 2.7–2.8 mW light intensity at the tip of fiber. The GC was calculated between two electrodes. Although LFP signals should have nonlinear relationships, it is very difficult to infer concrete nonlinear relationships from time-series. We focused only on the linear part of the relationships in this study, so that linear measures, the Granger causality and coherence, were employed.

Additional experiment was performed under two simultaneous recording from the septal and the temporal side of the hippocampus using single electrodes. In one situation, the photostimulation was applied in the septal side of the hippocampus to induce seizure-like afterdischarges (n = 5 rats, total 17 afterdischarges). In the other situation, the stimulation was applied in the temporal side of the hippocampus to induce seizure-like afterdischarges (n = 3 rats, total 18 afterdischarges). 10 Hz pulse stimulation was delivered for 30 seconds at a 10 ms pulse width (duty ratio 0.1) and a 2.7–2.8 mW light intensity at the tip of fiber. The GC was calculated between two electrodes.

LFP analysis

Preprocessing. The electrophysiological signals were band-pass-filtered between 1 and 300 Hz and down-sampled to 1 kHz for later analysis. All the following calculations were performed in MATLAB version 15 (MathWorks, Inc., Natick, MA).

Time-frequency analysis. The time-frequency representation of the LFP power was obtained by the wavelet transformation, with the Gabor mother wavelet defined by

\[ \psi(t) = g_s(t) \left( \exp(itf) - \exp(-\frac{\sigma^2 f^2}{2}) \right), \]

\[ g_s(t) = \frac{1}{2\sqrt{\pi}} \exp \left(-t^2/4\sigma^2\right), \]

where \( f \) is the central frequency, and \( \sigma = 5/f \).

Peak frequency was defined in the time-frequency distribution as the frequency with maximum power.

Granger causality, Granger index, and coherence. Degree of information flow was evaluated by Granger causality (GC) [27,28], where \( X(t) \) and \( Y(t) \) are two zero-mean stationary signals whose time observations are \( x_1(t) \) and \( y_2(t) \), with \( t = 1 \cdots T \). If the temporal dynamics of \( x_1(t) \) and \( x_2(t) \) could be written by an univariate autoregressive model of order \( p \), the model would be

\[ x_1(t) = \sum_{k=1}^{p} a_{11}(k)x_1(t-k) + u_1(t), \]

\[ x_2(t) = \sum_{k=1}^{p} a_{22}(k)x_2(t-k) + u_2(t), \]

where prediction error \( u_1(t) \) and \( u_2(t) \) for a signal depend only on its own past. \( x_1(t) \) and \( x_2(t) \) can be assumed to be represented by the following multivariate auto-regressive model of order \( p \),
\[ x_1(t) = \sum_{k=1}^{p} a_{11}(k)x_1(t-k) + \sum_{k=1}^{p} a_{12}(k')x_2(t-k') + w_1(t), \]

\[ x_2(t) = \sum_{k=1}^{p} a_{21}(k)x_1(t-k) + \sum_{k=1}^{p} a_{22}(k')x_2(t-k') + w_2(t), \]

where prediction error \( w_1(t) \) and \( w_2(t) \) depend on the past of the two signals. So in the model above, if \( w_1(t) \) were smaller than \( u_1(t) \), then we could conclude that \( X_2 \) caused \( X_1 \). Similarly, if \( w_2(t) < u_2(t) \), then \( X_1 \) caused \( X_2 \). In short, if knowing time series \( X_2 \) helped to predict the future of the other time series \( X_1 \) and \( X_2 \) “Granger caused” \( X_1 \). The magnitude of the GC was quantified by the log-ratio of the prediction error variance,

\[ G_{2 \rightarrow 1} = \ln \left( \frac{\text{var}(u_1)}{\text{var}(w_1)} \right). \]

The model order was chosen using Akaike’s information criterion (AIC) and Bayesian information criterion (BIC).

Dominance of the information flow, from septal side to temporal side or its opposite direction, was evaluated by an index, we called the “Granger index,” defined by

\[ \text{GrangerIndex} = \frac{G_{2 \rightarrow 1} - G_{1 \rightarrow 2}}{G_{2 \rightarrow 1} + G_{1 \rightarrow 2}}, \]

where \( G_{2 \rightarrow 1} \) and \( G_{1 \rightarrow 2} \) denote the GC from septal to temporal sides and the GC from temporal to septal sides, respectively. The Granger index, \( \epsilon [-1, 1] \), was positive if \( G_{2 \rightarrow 1} > G_{1 \rightarrow 2} \), otherwise it was negative. GC indicates positive values when the septal-to-temporal causality is larger than the opposite direction. Otherwise, it is negative.

We recorded the LFPs using a 16-channel multi-site probe, so we had \( 16 \times 16 \) LFP-pairs. To assess micro-scale causal relationships, widely separated LFP-pairs were excluded for Granger causality and Granger index. Only pairs whose distance was 450 μm or less (i.e., three times the inter-electrode interval or less) were used in calculation of the mean and the variance of the Granger causality, and the Granger index.

Coherence was introduced to evaluate the synchronization of signals in the frequency domain. The coherence of signals \( X_m(t) \) and \( X_n(t) \) was calculated as follows,

\[ \text{Coh}_{mn}(f) = \frac{|S_{mn}(f)|^2}{S_{mm}(f)S_{nn}(f)}, \]

\[ S_{mn}(f) = \frac{1}{2\pi} \int_{-\infty}^{\infty} C_{mn}(\tau) \exp(-j\tau)f\tau, \]

\[ C_{mn}(\tau) = X_m(t)X_n(t-\tau), \]

where overline \( \tau \) represents a temporal averaging operation, and \( S_{mn}(f) \) and \( C_{mn}(\tau) \) are the cross-spectrum and cross-correlation, respectively. The coherence is essentially the square of the correlation coefficient between the corresponding frequency component of \( X_m(t) \) and \( X_n(t) \).

In this study, we define the coherence by the average across frequencies:

\[ \text{Coherence} = \frac{1}{300-1} \int_{[0Hz]}^{[10Hz]} \text{Coh}_{mn}(f) df \]

For coherence, all the LFP-pairs were used for calculation of the mean and variance. The coherence quantifies the degree of synchrony in LFPs; 0 indicates complete asynchrony and 1 indicates complete synchrony.

The moving window. The GC and coherence were calculated using a 1000-ms-length moving window. The moving window moved in 100-ms time steps, so each window overlapped by 900 ms. The large overlapping was employed to draw the behavior of the GC and coherence in a sub-second temporal resolution. The center of moving window moved from \(-10\) seconds to 100 seconds around stimulus onset.

Transition on a state-space. The scatter plot clusters (Granger-index, coherence) were calculated by the k-means clustering method (k = 3 in this study) [29].

Results

Seizure-like afterdischarges were induced by repetitive photostimulation of the ChR2-expressing hippocampus

Seizure-like afterdischarges were successfully induced and reproduced by repetitive photostimulation to the hippocampus (Figure 2A). No rats died during the experiment. Seizure-like afterdischarges observed in this study were characterized as follows. During the initial stimulation phase, only evoked potentials followed each photostimulus pulse. High-amplitude spontaneous activity, which was not time-locked to stimuli, emerged in addition to the evoked potentials during stimulation and gradually became rhythmic and dominant (Figure 2B). This rhythmic activity self-persisted after the stimulation ended and spontaneously ceased in 8.4–85.5 (39.8±20.4; \( n = 115 \)) seconds. The afterdischarge duration was independent from stimulus frequency and duty ratio (two-way analysis of variance [ANOVA], p = 0.5). The seizure-like afterdischarge was associated with clonic twitches in the whiskers and paws and tonic conversion of the tail. Simultaneous LFP-electromyogram recordings revealed activation of brachial muscles, which never started earlier than afterdischarge (Figure 2C).

The self-sustained afterdischarges possessed frequency peaks around 10 and 25 Hz similarly after 10 Hz and 20 Hz photostimulation (Figure 3A). This frequency characteristic was common across as well as within animals (Figure 3B).

The chance of afterdischarge induction was dependent on the stimulus parameters. The highest rate was 1.0 (10 of 10 trials) observed at a 10 and 20 Hz pulse frequency and a smaller duty ratio of 0.05 (Figure 3C). Continuous stimulation did not efficiently induce afterdischarge (induction ratio = 0.1; data not shown). No clear refractory or facilitatory effect was observed on occurrence of afterdischarges in the 5 minutes interval stimulations. The number of induced afterdischarges was not statistically different between the first 10 trials and the last 10 trials (paired t-test, p = 0.425).

Afterdischarge induction was not due to an innate susceptibility of ChR2-TG animals to seizures. Repetitive photostimulation to the hippocampus of wild-type Wistar rats transfected with the rAAV-Chr2-Venus vector successfully reproduced seizure-like afterdischarges (Figure 4A-C). At least one afterdischarge was induced after photostimulation on any combinations of stimulus frequency (3, 10, 20 Hz) and duty ratio (0.05, 0.1, 0.2). The afterdischarge threshold was not significantly different (144±57.3
Figure 2. Electrical activities of optogenetically induced seizure-like afterdischarges. (A) Example traces of local field potentials recorded at the site of stimulation. Repetitive photostimulation at a 10 Hz frequency and a 0.05 duty ratio was applied to the hippocampus for 10 seconds by a hybrid-electrode fused with an optic fiber. The entire recording of the photostimulation and induced seizure-like afterdischarge is presented at the
top. Magnified views below corresponded to the numbers. Blue dots indicate photostimuli. At the start of stimulation, only evoked potentials followed each photo pulse (1). Spontaneous activities, which were not time-locked to stimuli, emerged in addition to the evoked potentials (2) and persisted after the stimulation ended (3). The activity gradually became high in amplitude and rhythmic (4,5) then stopped spontaneously (6). Note that waveform changes were observed even under stimulation (especially in A2). (B) Raster presentation of LFPs during and immediately after stimulation demonstrates that evoked responses are gradually replaced by non-time-locked activity. (C) Simultaneous recording of optogenetically induced afterdischarges and electromyogram (EMG) of the contralateral forelimb. Clonic EMG activities appeared during stimulation, but never persisted after the LFP afterdischarge.

Optic fiber insertion and photostimulation did not induce afterdischarges, by itself, in the absence of ChR2. No afterdischarges were observed after repetitive pulse photostimulation of the "normal" hippocampus in wild-type Wister rats. The chance charges were observed after repetitive pulse photostimulation of afterdischarges, by itself, in the absence of ChR2. No afterdischarges were observed after repetitive pulse photostimulation of afterdischarges, by itself, in the absence of ChR2. It should be noted that seizure-like afterdischarge was induced one out of 10 trials after the stimulation of the sensori-motor cortex.

# Induced seizure-like afterdischarge activated the entire hippocampus

The c-Fos expression was induced in the entire hippocampus of ChR2V-TG rats after a single seizure-like afterdischarge induced by pulse photostimulation (Figure 5A, Figure S1). % c-Fos positive cell was significantly higher in the afterdischarge group than in the no-afterdischarge group (two-way ANOVA, p<0.0001). No significant differences were observed in the % c-Fos positive cell between septal and temporal hippocampus (p=0.90) (Figure 5B). The c-Fos expression was proportional among hippocampal subregions in seizure group (p<0.01 in CA3 vs. DG, p=0.043 in CA3 vs. CA1) (Figure S2A, B).

Bidirectional and asymmetric causal relationships were observed along the septo-temporal axis of the hippocampus during seizure-like afterdischarges

Multisite LFP recording revealed that induced seizure-like afterdischarges were characterized by an increase in the GC along the ST hippocampus (Figure 6A). During hippocampal stimulation, the GC indices increased in both the septal-to-temporal and temporal-to-septal directions, but were higher in the former (Figure 6B, top panels). The Granger index quantified the dominant direction (Figure 6B, middle panels; see Methods for details). The Granger index is positive if the septal-to-temporal is the dominant direction. Otherwise it is negative. In the course of self-sustained afterdischarges after stimulation ended, the septal-to-temporal GC gradually decreased to the same level as the temporal-to-septal GC. Toward the final phase, the GC indices again increased in both directions, and the temporal-to-septal GC became higher in comparison. The seizure-like afterdischarge was also characterized by an increase in coherence (Figure 6B, bottom panels). Zero indicates complete asynchrony and 1 indicates complete synchrony of LFPs. The coherence showed a gradual increase toward the end of the afterdischarge and vanished at afterdischarge termination. An example of GC and coherence matrix was presented in Figure S3. Granger causality did not depend on the distance between electrode pair, but rather on their relative position. Increase of the septal-to-temporal causality tended to occur in electrode pairs in the septal side, while increase of the temporal-to-septal causality did in the temporal side. Higher coherence was seen in closer pairs of electrodes.

The above changes in GC were not a simple propagation of activity from the stimulation site to the other. Increase of

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**Figure 3. Characteristics of optogenetically induced seizure-like afterdischarges.** (A) Average curve of frequency spectrum for the first 10 seconds of the induced afterdischarge after photostimulation. Seizure-like afterdischarges possessed frequency peaks around 10 and 25 Hz similarly after 10 Hz (blue) and 20 Hz (red) photostimulation. The duty ratio was 0.05 in both. The power spectral density curve was an average of 10 afterdischarges recorded from 10 rats. This also indicates that the frequency characteristic was common across animals. (B) Average curve of frequency spectrum of the first 10 seconds of afterdischarges recorded in a single animal. The power spectral density curve was an average of 10 afterdischarges including 4, 5, and 1 afterdischarges after 10, 20 and 40 Hz photostimulations respectively with various duty ratios. Seizure-like afterdischarges showed frequency peaks around 10 and 25 Hz. (C) Chance of afterdischarge induction is plotted against stimulus frequency and duty ratio (n=115 seizures, n=10 rats). The highest chance was 1.0 (10 afterdischarges induced in 10 trials) observed with 10 and 20 Hz stimulus frequencies and a duty ratio of 0.05. Optical intensity was 19–22 mW at the tip of optic fiber and stimulus duration was 10 seconds.

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Figure 4. Afterdischarge induction was not due to an innate susceptibility of ChR2V-TG animals to seizures. (A) AAV5-ChR2V viral vector was injected to rat hippocampus 4 weeks prior to the afterdischarge induction experiment (n = 3). (B) Fluorescent images of ChR2V protein (green) expression in fibers running through the hilus, the molecular layer of the dentate gyrus, and the striatum radiatum of CA3. (C) Raw waveform recorded in the hippocampus during afterdischarge induction. Repetitive photostimulation induced seizure-like afterdischarge similar to that observed in the experiment using ChR2V-TG rats. At least one afterdischarge was induced after photostimulation on any combinations of stimulus frequency (5, 10, 20 Hz) and duty ratio (0.05, 0.1, 0.2). Optical intensity and stimulus duration were fixed at 19–22 mW at the tip of optic fiber and at 20 seconds, respectively. (D) Electrical stimulation was delivered to induce “classical” afterdischarge in the hippocampus. No significant difference was observed in the afterdischarge threshold between ChR2V-TG rats (n = 5) and wild-type Wistar rats (n = 5), suggesting that no inherent excitability existed in the transgenic rats. (B) Repetitive pulse photostimulation was delivered to the hippocampus and extra-hippocampal structures in ChR2V-TG rats (n = 4). The chance of afterdischarge induction was very low or zero in the amygdala, anterior thalamic nucleus and sensorimotor cortex. Stimulation parameters were set at 10 Hz with a duty ratio of 0.05. Optical intensity and stimulus duration were fixed at 19–22 mW at the tip of optic fiber and at 10 seconds, respectively. It should be noted that seizure-like afterdischarge was induced one out of 10 trials after the stimulation of the sensori-motor cortex. doi:10.1371/journal.pone.0060928.g004
septal-to-temporal GC was observed both during the septal and temporal stimulations in the additional experiment with two simultaneous recording (Figure 7).

A state-space plot between the Granger index and coherence indicated the presence of at least three attractors by the k-means clustering (Figure 6C): 1) a resting state before and after the afterdischarge; 2) afterdischarge initiation with moderate coherence and dominant septo-temporal GC; and 3) afterdischarge termination with increased coherence and dominant temporo-septal GC. These changes were present across animals.

**Discussion**

Repetitive pulse photostimulation to the ChR2-expressing rodent hippocampus reproducibly induced seizure-like afterdischarges, which was self-sustained and propagated through the entire hippocampus. This phenomenon was confirmed in both ChR2-VTG rats and wild-type Wistar rats transfected with AAV5-ChR2V vectors. Afterdischarge induction was most efficient at 10 and 20 Hz stimulus frequencies with a smaller duty ratio, and the induced afterdischarges were stereotypical in terms of frequency characteristics and duration. Simultaneous recording of multisite LFPs revealed bidirectional and asymmetric causal relationships along the ST axis of the hippocampus during genesis and termination of seizure-like afterdischarges. State-space representation of causality and coherence indicated three discrete states of the phenomenon: 1) resting state; 2) afterdischarge initiation with moderate coherence and dominant septo-temporal causality; and 3) afterdischarge termination with increased coherence and dominant temporo-septal causality.
Figure 6. Causal relationships and coherences were dynamically changed along the septo-temporal axis of the hippocampus during seizure-like afterdischarges. (A) Pulse photostimulation was delivered to the septal hippocampus, and induced afterdischarges were simultaneously recorded from multi-contact electrodes inserted along the septo-temporal axis of the temporal hippocampus (n = 3 rats). (B) Time courses of Granger causality, Granger index, and coherence are shown for both a single induced afterdischarge and a population average of afterdischarges (10 afterdischarges per rat, total 30 afterdischarges). On the population average, the thick line and shaded areas indicate the mean and 99.9% confidence interval, respectively. The average and standard deviation were calculated from the recorded LFPs of 30 trials of three rats (total 1620 LFP-pairs). The Granger causality increased in both directions but was greater in the septo-temporal direction at afterdischarge initiation. Temporo-septal causality became higher toward the end of the afterdischarge, causing transition of the Granger index to a negative value.
Coherence was gradually increased toward the end of the afterdischarge. (C) State-space plots of Granger index and coherence. The population average (right) shows the mean of 30 afterdischarges. K-mean clustering ($k = 3$) revealed three distinct states: 1) resting state in which causality and synchrony were both low (black); 2) early phase of afterdischarge characterized by dominant septo-temporal causality and increase in coherence (red); and 3) late phase of afterdischarge characterized by reversal of causality index to the temporo-septal direction and increase in coherence (green). Transitions between phases are indicated by arrows.

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Optogenetics for a novel model of seizure-like afterdischarges

The current study proposes a novel optogenetic methodology to induce seizure-like afterdischarges in vivo animals with photosimulation to the local hippocampus circuits. Epilepsy is one of the most common neurological disorders that can involve any part of the central nervous system [30], and the hippocampus is a major site that generates focal seizures in humans, particularly in those with drug-resistant epilepsy [4]. Although most previous studies employed optogenetics for precise and specific control of neurons, here, we applied the technique to perturb the hippocampal network and subsequently reproduce a disease state.

Our novel method of afterdischarge induction is advantageous in its reproducibility, low mortality (almost zero) and artifact-free electrophysiological observations, compared with conventional models of seizures. Repetitive electrical stimulation of the brain has long been known to induce “epileptiform” discharges, especially in the hippocampus [11,31,32]. Here we applied optogenetic approach instead of electrical stimulation for seizure induction. To the best of our knowledge, optogenetics have not been used for development of a model of epileptic disorders.

Figure 7. Causality analysis of LFPs in S-T axis of hippocampus in septal and temporal stimulations. (A,B) Schematic of experimental set-up used for two simultaneous recording and the septal and temporal hippocampal photostimulation ($n = 3$, total 17 seizures). (C, D) Traces of bidirectional Granger causality (GC) scores from recorded LFPs in the stimulation to the septal (C) and temporal (D) hippocampus. (Top panels) Example traces of the GC scores. (Middle panels) Average traces of bidirectional GC scores, among three trials in one rat (septal stimulation) and seven trials of one rat (temporal stimulation). Colored regions indicate 95% confidence interval. (Bottom panels) The same as the middle panels, but the average traces were calculated using 17 trials of three rats (septal stimulation) and 18 trials of three rats (temporal stimulation). Increase of septal-to-temporal GC was observed both during the septal and temporal stimulations.

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advantage of our approach is artifact-free observation of electrophysiology during stimulation. LFPs were successfully recorded and analyzed during stimulation to reveal spatio-temporal dynamics of seizure-like afterdischarge. The artifact-free electrophysiological recording during stimulation provides a valuable opportunity to study neurophysiological processes of seizure genesis.

Many other acute seizure models have been developed by altering cortical excitability, such as topical application of penicillin, systemic or local administration of kainic acid [6]. The advantage of electrical or optogenetic stimulation is replication of seizures without minimum histological damages. Ten or more seizure-like afterdischarges can be reproduced in one rat without mortality using this model. The model is suitable to investigate neural networks that maintain seizure activity and secondary effect of epileptic seizures.

It should be noted here that this is a model of epileptic seizures, rather than epilepsy. Models of epilepsy, the model that spontaneously generates epileptic seizures, would be more relevant to study epileptogenesis [6,9]. However, a model of epileptic seizures is still important in understanding its mechanisms of genesis, because many current therapeutics are developed to suppress or counteract epileptic seizures [7]. Efficient induced-seizure model is applicable for evaluating the efficacy of epilepsy therapeutics [33]. Anti-seizure efficacy could be measured as a probability of afterdischarge induction in a short time.

Currently it is difficult to determine what subpopulation of hippocampal neurons was activated to trigger seizure-like afterdischarges in this experiment. In our model, ChR2 was expressed non-selectively both in pyramidal neurons and interneurons. According to previous reports, penetration depth of light would range in an order of hundred μm or 1 mm [34,35]. Theoretically, the optical stimulation activation threshold depends on ChR2 channel density and surface area [36], implying that optical stimulation mainly acts on cell body, but also on passing fibers to some extent. Besides pyramidal neurons, interneurons with higher input resistance may respond more easily to ChR2 depolarization. One previous study showed that optogenetic stimulation of the mouse neocortex expressing ChR2 could produce the evoked LFP similar to electrical stimulation [37]. Thus, it is possible that subsequent activation process would be similar between optogenetic and electrical stimulation. To further understand mechanisms of seizure-genesis, advanced strategy is necessary, including selective introduction of ChR2 to excitatory neurons or to inhibitory neurons, use of hyperpolarizing channels such as Halorhodopsin (NpHR), and anatomically selective application of photostimulus.

**The septo-temporal network is important in hippocampal seizure-genesis**

Seizure genesis is characterized by its diffuse and dynamic nature. When observed using LFPs, seizure activity is initiated diffusely or focally in different locations in the hippocampus, and the onset patterns can be different among seizure in a single subject [10]. Once initiated, focal seizure activity is propagated along not only the transverse but also the septo-temporal (longitudinal) direction of the hippocampus, and the propagation pattern can be bidirectional in a single seizure [38].

Importance of the septo-temporal connections in seizure propagation has already been investigated [38–40]. Derchansky et al examined latencies of waveform peaks in multi-site LFPs along the septo-temporal axis of hippocampus during seizures using low-magnesium model and focal tetanic stimulation model of isolated hippocampus [38]. In the low-magnesium model, epileptiform discharges always started from ventral hippocampus, but propagation direction can “flip” several times in later course of seizures. In the focal tetanic stimulation model, epileptiform discharges always propagated from the stimulation site to the other, and similar bidirectional propagation followed. Interestingly, they noted the flip pattern can be independent between low (<10 Hz) and high frequency components. Our results further support those previous data on the septo-temporal interaction in seizure genesis. We showed bidirectional changes in information flow during seizure-like afterdischarges similarly with Derchansky’s study, while our study used in vivo model and different measures. Using Granger causality, we showed that the septo-temporal interaction was not a simple propagation of the activity from the stimulation to the other. Both in the septal and temporal stimulations, increase of septal-to-temporal GC was observed during afterdischarges.

Long-range direct connection is relatively scarce along the hippocampal septo-temporal axis, in spite of the potential role in seizure dynamics. Filipe et al studied septo-temporal propagation of afterdischarges caused by electrical stimulations [39]. They investigated both linear and non-linear measures for association, and the value of association was generally larger in non-linear than linear method. Larger association was found between ipsi- and contra-lateral septal hippocampus than between the septal and temporal hippocampus. Relatively low association noted in Filipe’s study is probably explained by long distance between recording sites for comparison, i.e. septal and temporal hippocampus. In such situation, they found that non-linear measures were better than linear ones to detecting associations. Linear association was better investigated in short-range comparison using multi-site LFP recording, like in our study and Derchansky’s report. This implicates that long and direct association fibers are relatively few in the septo-temporal direction compared with commissural connections [39].

Behaviors of dynamic and highly interacting systems, such as the central nervous system (CNS), are investigated from the viewpoint of non-linear complex systems [41]. Occurrence of epileptic seizures has been interpreted as a transition between bi- or multi-stable states of neuronal networks (i.e., normal or “interictal” states versus epileptic or “ictal” states) [42]. The theory of non-linear dynamics has frequently been applied to the human electroencephalogram (EEG) and used as an early warning sign before seizure transition [42,43]. The theory is also used for better understanding the spatio-temporal dynamics of seizure [43,44].

Bidirectional causal relationships revealed by GC analysis suggest the presence of hierarchical network dynamics along the longitudinal axis of the hippocampus in generating, maintaining and terminating seizures. The GC analysis was previously applied to an absence epilepsy model, in which the thalamo-cortical recurrent network is responsible for seizure genesis. A bidirectional increase in causality was observed during seizures, but the intensities and time courses of the two causalities were asymmetrical (i.e., the thalamo-frontal causality was more intensive, and the fronto-thalamo causality was restored to the initial level before seizure cessation) [45]. Two classes of network associations were hypothesized: “driving” and “modulating” connections during seizures based on the “no-strong-loop” hypothesis of recurrent neuronal networks [46]. Bidirectional causal relationships in epileptic seizures were also demonstrated in the lamellar organization of the hippocampal network. The GC from the CA1 subfield to the dentate gyrus was increased prior to and during seizure, and causality reversal occurred before seizure cessation [44]. The bidirectional causal relationships observed in our study suggest the presence of hierarchical and asymmetrical...
induction with low mortality. Induction in a short time, due to acute and reliable afterdischarge efficacy could be measured as a probability of afterdischarge antiepileptic drugs or other therapeutics for epilepsy. Moreover, this model is applicable to evaluating the efficacy of fact-free electrophysiological recording, providing a valuable method of afterdischarge induction enabled simultaneous arti-
charges in the hippocampus using optogenetics. This novel in seizure genesis (Figure 8) [43,44].

From an anatomical standpoint, the hippocampal cell population and their synaptic connections are not symmetrical between subregions along the longitudinal axis [47]. Packing densities of granule cells and CA3 pyramidal cells vary along the ST axis [48], suggesting that the hippocampal longitudinal circuit is not a simple recurrent circuit. Moreover, the septal, intermediate, and temporal parts of the hippocampus display distinctive patterns of connectivity to extra-hippocampal structures [49]. Thus, the above features also support the asymmetrical dynamics of seizures along the ST axis of the hippocampus.

Conclusions and Perspectives

We developed a novel in vivo model of seizure-like afterdischarges in the hippocampus using optogenetics. This novel method of afterdischarge induction enabled simultaneous artifact-free electrophysiological recording, providing a valuable opportunity to study neurophysiological processes of seizures. Moreover, this model is applicable to evaluating the efficacy of antiepileptic drugs or other therapeutics for epilepsy. Anti-seizure efficacy could be measured as a probability of afterdischarge induction in a short time, due to acute and reliable afterdischarge induction with low mortality. Our findings provide additional evidence for the potential role of the longitudinal hippocampal network in seizure dynamics. Bidirectional networks along the ST axis of the hippocampus are engaged in a hierarchical fashion during generation and termination of seizure-like afterdischarges. A better understanding of seizure dynamics will aid in developing new treatments for epileptic seizures (e.g., selective blockade of the network engaged in seizure genesis).

Supporting Information

Figure S1 c-Fos expression in the induced seizure-like afterdischarge. (A) c-Fos expression in a control rat with no induced afterdischarges. Minimum amount of expression was seen. (B) c-Fos expression at the stimulation site in a rat with induced afterdischarge. (C) c-Fos expression at the temporal hippocampus away from the stimulation site in a rat with induced afterdischarge. Strong c-Fos expression was also seen in the temporal hippocampus.

Figure S2 Hippocampal subregions are activated in parallel by optogenetically induced seizure-like afterdischarges. Proportions of neurons expressing the immediate early gene, c-Fos in the afterdischarge-induced group (A) and the control group (B). % c-Fos positive cells in DG and CA1 are plotted against CA3. (A) The level of c-Fos expression in CA3 was correlated with that of DG (p<0.01) and CA1 (p = 0.043) in the afterdischarge group. (B) The % c-Fos positive cell was low in the control group.

Figure S3 Examples of the Granger causality and coherence. Example traces of the Granger causality and coherence (rat 0624, trial 17). The numbers (1 to 16) at the left and upper part of the figure indicate the index of the recording sites on the probe. The site 1 is in the septal side of the hippocampus and nearest to the stimulation site. The site 16 is in the temporal side of the hippocampus and farthest to the stimulation site. The LFPs were recorded from these 16 recording sites (Recording site 2 is broken in this example experiment). The Granger causality and coherence were calculated in all LFP pairs. Right-upper panels are the Granger causality of the LFP pairs. The red line indicates the causality from temporal to septal direction. The blue line indicates the causality from septal to temporal direction. The left-lower panels are the coherence of the LFP pairs. The horizontal axis is time (second) for all panels. The photostimulation was applied from 10 to 40 seconds. Granger causality did not depend on the distance between electrode pairs, but rather on their relative position. Increase of the septal-to-temporal causality tended to occur in electrode pairs in the septal side, while increase of the temporal-to-septal causality did in the temporal side. Higher coherence was seen in closer pairs of electrodes.

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Author Contributions

Conceived and designed the experiments: HM MI SO RH HY. Performed the experiments: SO RH YM HT TI ES MI. Analyzed the data: SO RH MI EO HM. Contributed reagents/materials/analysis tools: RH EO HM. Wrote the paper: SO HM RH NN TT.

References

1. Traub RD, Wong RK (1982) Cellular mechanism of neuronal synchronization in epilepsy. Science 216: 745–747.
2. Fisher RS, Van Emde Boas W, Blume W, Elger C, Genton P, et al. (2005) Epileptic seizures and epilepsy: definitions proposed by the International League Against Epilepsy (ILAE) and the International Bureau for Epilepsy (IBE). Epilepsia 46: 470–472.
3. Jefferys JG (1990) Basic mechanisms of focal epilepsies. Exp Physiol 75: 127–162.
4. Wieser H-G (2004) ILAE Commission Report. Mesial temporal lobe epilepsy with hippocampal sclerosis. Epilepsia 45: 695–714.
5. Wiebe S, Blume WT, Givin JP, Eliazuw M (2001) A randomized, controlled trial of surgery for temporal-lobe epilepsy. New Eng J Med 345: 311–318.
6. Raol YH, Brooks-Kayal AR (2012) Experimental models of seizures and epilepsies. Prog Mol Biol Trans Sci 105: 57-82.

7. De Curtis M, Gnattovsky V (2009) Reevaluating the mechanisms of focal isogenesis: The role of low-voltage fast activity. Epilepsia 50: 2314-2325.

8. Avoli M, De Curtis M, Kohling R (2012) Does interstitial synchronization influence isogenesis? Neuropharmacology: 1-8.

9. Goddard G V (1967) Development of epileptic seizures through brain stimulation at low intensity. Nature 214: 1020-1021.

10. Bertram EH (1997) Functional anatomy of spontaneous seizures in a rat model of limbic epilepsy. Epilepsia 38: 95-105.

11. Lothman EW, Williamson JM (1992) Influence of electrical stimulus parameters on afterdischarge thresholds in the rat hippocampus. Epilepsy Res 13: 205-213.

12. Spencer SS, Guimarães P, Katz A, Kim J, Spencer D (n.d.) Morphological patterns of seizures recorded intracranially. Epilepsia 33: 537-545.

13. Bartolomei F, Chauvel P, Wesseling F (2008) Epileptogenesis of brain structures in human temporal lobe epilepsy: a quantified study from intracranial EEG. Brain 131: 1818-1830.

14. Huberfeld G, Menenédez de la Prida I, Pallidó J, Cohen I, Le Van Quyen M, et al. (2011) Glutamatergic pre-ictal discharges emerge at the transition to seizure in human epilepsy. Nat Neurosci 14: 627-634.

15. Tye KM, Deisseroth K (2012) Optogenetic investigation of neural circuits underlying brain disease in animal models. Nat Rev Neurosci 13: 251-266.

16. Paz JT, Bryant AS, Peng K, Fenno L, Yizhar O, et al. (2011) A new mode of corticothalamic transmission revealed in the Gria4(-/-) model of absence epilepsy. Nat Neurosci 14: 1167-1173.

17. Kvaritz A V, Freeze BS, Parker PRL, Kay K, Thiwin MT, et al. (2010) Regulation of parkinsonian motor behaviours by optogenetic control of basal ganglia circuitry. Nature 466: 622-626.

18. Tounes J, Sörensen AT, Deisseroth K, Lundberg C, Kokaia M (2009) Optogenetic control of epileptiform activity. Proc Nat Acad Sci U S A 106: 12162-12167.

19. Ledri M, Nikádhól I, Erdélyi F, Szabo G, Kiké D, et al. (2012) Altered profile of basket cell afferent synapses in hyper-excitabilite dentate gyrus revealed by optogenetic and two-pathway stimulations. Eur J Neurosci 36: 1971-1983.

20. Yizhar O, Fennó LE, Davidson TJ, Mogri M, Deisseroth K (2011) Optogenetic in neural systems. Neuron 71: 9-34.

21. Gradinaru V, Thompson KR, Zhang F, Mogri M, Kay K, et al. (2007) Targeting and readout strategies for fast optical neural control in vitro and in vivo. J Neurosci 27: 14231-14238.

22. Tomita H, Sugano E, Fukaiwa Y, Isago H, Sugiyama Y, et al. (2009) Visual Properties of Transgenic Rats Harboring the Channelrhodopsin-2 Gene Regulated by the Thy-1.2 Promoter. PLoS ONE 4: e7679.

23. Ji ZG, Ito S, Honjoh T, Ohta H, Ishizuka T, et al. (2012) Light-evoked somatoasynaptic perception of transgenic rats that express channelrhodopsin-2 in dorsal root ganglion cells. PLoS ONE 7: e32699.

24. Sugano E, Isago H, Wang Z, Murayama N, Tama M, et al. (2011) Immune responses to adeno-associated virus type 2 encoding channelrhodopsin-2 in a genetically blind rat model for gene therapy. Gene Ther 18: 266-274.

25. Inoue T, Yamashita Y, Nishihara M, Sugiyama S, Sonoda Y, et al. (2009) Therapeutic efficacy of a polymeric micellar doxorubicin infused by convection-enhanced delivery against intracranial 9L brain tumor models. Neuro Oncol 11: 1928–1936.

26. Paxinos G, Watson C (2007) The Rat Brain in Stereotaxic Coordinates. 6th ed. Academic Press.

27. Granger CWJ (1969) Investigational Causal Relations by Econometric Models and Cross-Spectral Methods. Econometrica 37: 424-438.

28. Seth AK (2010) A MATLAB toolbox for Granger causal connectivity analysis. J Neurosci Methods 186: 262-273.

29. MacQueen J (1967) Some methods for classification and analysis of multivariate observations. Proc Fifth Berkeley Symp Math Statist Prob 1: 281-297.

30. Sander JW, Shorvon SD (1996) Epidemiology of the epilepsies. J Neurol Neurosurg Psychiatry 61: 433-443.

31. Stringer JL, Williamson JM, Lothman EW (1989) Induction of paroxysmal discharges in the dentate gyrus: frequency dependence and relationship to afterdischarge production. J Neurophysiol 62: 126–135.

32. Shigeto H, Boongird A, Baker K, Kellinghaus C, Najm I, et al. (2012) Systematic study of the effects of stimulus parameters and stimulus location on afterdischarges elicited by electrical stimulation in the rat. Epilepsy Res 1 9–1.

33. Albus K, Wahab A, Heinemann U (2012) Primary afterdischarge in organotypic hippocampal slice cultures: Effects of standard antiepileptic drugs. Epilepsia 53: 1928-1936.

34. Yaroslavsky AN, Schulze PC, Yaroslavsky I V, Schober R, Ulrich F, et al. (2002) Optical properties of selected native and coagulated human brain tissues in vitro in the visible and near infrared spectral range. Phys Med Biol 47: 2093-2073.

35. Zhang F, Gradinaru V, Adamantidis AR, Durand R, Auran RD, et al. (2010) Optogenetic interrogation of neural circuits: technology for probing mammalian brain structures. Nat Protoc 5: 439-456.

36. Foutz TJ, Arlow RL, McIntyre CG (2012) Theoretical principles underlying optical stimulation of a channelrhodopsin-2 positive pyramidal neuron. J Neurophysiol 107: 3235-3245.

37. Xiong W, Jin X (2012) Optogenetic field potential recording in cortical slices. J Neurosci Methods 210: 119-124.

38. Derchansky M, Rotki D, Rick JF, Wernberg R, Barabakian BL, et al. (2006) Bidirectional multistate seizure propagation in the intact isolated hippocampus: the multifacility of the seizure “focus”. Neurobiol Dis 23: 312-328.

39. Filipé CN, Pijp JP, De Lima VM, De Silva FH (1989) Propagation of afterdischarges along the septo-temporal axis of the rat hippocampus: a quantitative analysis. Electroencephalogr Clin Neurophysiol 73: 172-178.

40. Pallidó J, Hausser U, Langlois M, Hamelin S, Devaux B, et al. (2012) Dentate gyrus and hilus transaction blocks seizure propagation and granule cell dispersion in a mouse model for mesial temporal lobe epilepsy. Hippocampus 21: 334–343.

41. Scheffler M, Bascombe J, Brock WA, Brovkin V, Carpenter SR, et al. (2009) Early-warning signals for critical transitions. Nature 461: 53-59.

42. Lopes da Silva F, Blanes W, Kuziuk SN, Parra J, Soffczynski P, et al. (2003) Epilepsies as dynamical diseases of brain systems: basic models of the transition between normal and epileptic activity. Epilepsia 44 Suppl 1: 72-83.

43. Jasemidis LD, Shau D-S, Sackleres JC, Pardalos PM, Prasad A (2004) Dynamical resetting of the human brain at epileptic seizures: application of nonlinear dynamics and global optimization techniques. IEEE Trans Biomed Eng 51: 495–506.

44. Cadotte AJ, DeMarz TB, Marcey TH, Parche MB, Talathi SS, et al. (2010) Granger causality relationships between local field potentials in an animal model of temporal lobe epilepsy. J Neurosci Methods 189: 121–129.

45. Shutkova E, Dikanov T, Smirnov D, Bezrucho B, Van Luijtelaar G (2008) Granger causality: cortico-thalamic interdependencies during absence seizures in WAG/Rij rats. J Neurosci methods 170: 245–254.

46. Crick F, Koch C (1998) Constraints on cortical and thalamic projections: the no-strong-loops hypothesis. Nature 391: 245-250.

47. Ammaral DG, Lavenex P (2007) Hippocampal Neuroanatomy. In: Andersen P, Morris R, Warland K, editors. The Hippocampus Book. New York: Oxford University Press. pp. 37–114.

48. Gaarskjaer FB (1986) The organization and development of the hippocampal subiculum in the WAG/Rij rats. J Neurosci methods 170: 245–254.

49. Fanselow MS, Dong H-W (2010) Are the dorsal and ventral hippocampus functionally distinct structures? Neuron 63: 7–19.