Data Article

ECG waveform dataset for predicting defibrillation outcome in out-of-hospital cardiac arrested patients

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\textbf{A R T I C L E   I N F O}

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\textbf{A B S T R A C T}

The provided database of 260 ECG signals was collected from patients with out-of-hospital cardiac arrest while treated by the emergency medical services. Each ECG signal contains a 9 second waveform showing ventricular fibrillation, followed by 1 min of post-shock waveform. Patients’ ECGs are made available in multiple formats. All ECGs recorded during the prehospital treatment are provided in PFD files, after being anonymized, printed in paper, and scanned. For each ECG, the dataset also includes the whole digitized waveform (9 s pre- and 1 min post-shock each) and numerous features in temporal and frequency domain extracted from the 9 s episode immediately prior to the first defibrillation shock. Based on the shock outcome, each ECG file has been annotated by three expert cardiologists, - using majority decision - , as successful (56 cases), unsuccessful (195 cases), or indeterminable (9 cases). The code for preprocessing, for feature extraction, and for limiting the investigation to different temporal intervals before the shock is also provided. These data could be reused to design algorithms to predict shock outcome based on ventricular fibrillation analysis, with the

\textsuperscript{*} Data Availability: Cardially - ECG waveform dataset for predicting defibrillation outcome in out-of-hospital cardiac arrested patients (Original data) (Mendeley Data)

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Specifications Table

| Subject                           | Cardiology and Cardiovascular Medicine |
|-----------------------------------|----------------------------------------|
| Specific subject area             | Quantitative analysis of ECG waveform in out-of-hospital cardiac arrested patients to guide and optimize resuscitation protocols |
| Type of data                      | Table (.TXT format, .XLS format) Graph (.PDF format) |
| How data were acquired            | Semiautomatic Heartstart 3000 defibrillator (Laerdal Medical, Stavanger, Norway) |
| Data format                       | Raw Analysed Filtered                   |
| Parameters for data collection    | ECG and all relevant demographic information were recorded according to the Utstein guidelines [1]. |
| Description of data collection    | The ECG data were collected from 260 patients with out-of-hospital cardiac arrest treated by the emergency medical services according to the 2005 European CPR guidelines [2]. The defibrillation electrodes were placed onto the patient’s torso to comply with a standard lead II configuration. |
| Data source location              | Institution: University of Brescia City/Town/Region: Brescia Country: Italy |
| Data accessibility                | Repository name: Mendeley Data Data identification number: DOI: https://doi.org/10.17632/wpr5nzyn2z.1 Direct URL to data: https://doi.org/10.17632/wpr5nzyn2z.1 |
| Related research article         | Author’s name: Marija D. Ivanović, Julius Hannink, Matthias Ring, Fabio Baronio, Vladan Vukčević, Ljupco Hadžievski, and Bjoern Eskofier Title: Predicting defibrillation success in out-of-hospital cardiac arrested patients: Moving beyond feature design [4] Journal: Artificial Intelligence in Medicine (ISSN: 0933–3657) DOI: https://doi.org/10.1016/j.artmed.2020.101963. |

Value of the Data

- The data can be used by both computer scientists and physicians to perform quantitative analysis of ECG waveform.
- The data are useful to develop models and classification strategies to predict the defibrillation outcome of out-of-hospital cardiac arrested patients.
- By evaluating the likelihood of a successful defibrillation outcome the optimal timing of delivering the shock can be determined avoiding defibrillation attempts with low probability of success in favour of CPR and chest compression.
- The developed models and algorithms could be made available in the current automated external defibrillators to guide resuscitation protocols with respect to the condition of the patient.
Fig. 1. ECG waveform of subject 12,999 in ventricular fibrillation which returns to ROEA after the defibrillation. In evidence the arming (first row), the delivery of the first shock (second row), and the return of an organized electrical activity (third row).

1. Data Description

1.1. ECG original files

The 260 patients’ ECGs recorded during prehospital treatment by the emergency medical services have been first anonymized, then printed in paper, scanned, and finally converted to electronic PDF files. These data contain 9 s of pre-shock waveform and 1 min of post-shock signal. As one of the novelties with respect to data used in our previous publication [3,4], we make here available all the 260 original ECG signals as PDF electronic files. Out of the 260 ECGs, 56 have been categorized by expert cardiologists, using majority voting, as successful (ROEA, i.e., return of an organized electrical activity), 195 as unsuccessful (NoROEA), and 9 as indeterminable. An example of a PDF file containing the ECG waveform with ROEA is presented in Fig. 1.

1.2. Digitized ecg waveforms

We make also available the 260 patients’ ECGs in digitized forms, with ECG amplitude time-courses reported in textual files (.txt). As for the electronic PDFs, each ECG signal contains 9 s of pre-shock and 1 min of post-shock ECGs. However, the textual file of different patients may have different number of samples since the Findgraph software [5], used to convert the graphs in textual form, non-uniformly samples traces in the temporal coordinate. As example of the digitized version of a pre-shock ECG waveform (which is the digitized version of Fig. 1, first row) is given in Fig. 2.

1.3. Extracted features

Features have been extracted from the 9 s episode immediately prior to the first defibrillation shock on each patient, whereas in our previous publication [3], feature were computed on a 4 s episode prior to the first shock. The code used for preprocessing and feature extraction is
Table 1
Extracted features and the references where they are defined, when available.

| Time Domain | Frequency Domain | Wavelet Domain | Non-linear Dynamic |
|-------------|------------------|----------------|--------------------|
| RMS [7]     | AMSAabs [6]      | LBE [11]       | PSDR [n.a.]        |
| SA [8]      | PSA [6]          | MBEn [11]      | PAREA [n.a.]       |
| MA [6]      | ENRG [6]         | HBEn [11]      | MSI [12]           |
| WA [8]      | CF [6]           |                | ApEn [13]          |
| AmpMax [n.a.] | CP [6]      |                | ShEn [7]           |
| AmpMin [n.a.] | DF [7]     |                | H [9]              |
| PTT [6]     | EF [10]          |                | DFA [11]           |
| PPA [6]     | SFM [6]          |                |                    |
| MedS [6]    |                  |                |                    |
| MS [6]      |                  |                |                    |

Table 2
Average values of features in the time domain for ROEA vs. NoROEA patients.

| Feature      | NoROEA     | ROEA       |
|--------------|------------|------------|
| RMS (mV)     | 0.152898   | 0.233713   |
| SA (μV)      | 9.256636   | 10.347003  |
| MA (mV)      | 0.120922   | 0.184623   |
| WA (mV)      | 0.314829   | 0.468969   |
| AmpMax (mV)  | 0.447482   | 0.686967   |
| AmpMin (mV)  | −0.465381  | −0.698427  |
| PTT (mV)     | 0.912863   | 1.385395   |
| PPA (mV)     | 0.612459   | 0.927987   |
| MS (mV/s)    | 0.019300   | 0.025711   |
| MedS (mV/s)  | 0.164440   | 0.623704   |

also available, and can be parameterized to different temporal intervals. The features we provide can be categorized in four groups. With respect to time domain, we have features of waveform amplitude, phase, and slope:

- root mean square (RMS)
- average segment amplitude (SA)
- mean amplitude (MA)
- wave amplitude (WA)
- maximum amplitude (AmpMax)
- minimum amplitude (AmpMin)
- amplitude range, or peak-to-through (PTT)
- average peak-to-peak amplitude (PPA)
- median slope (MedS)
- mean slope (MS)
Fig. 3. Distribution of samples measured for the time-domain features, distinct for the two groups ROEA and NoROEA: a) RMS, b) SA, c) MA, d) WA, e) AmpMax, f) AmpMin, g) PTT, h) PPA i) MS, and j) MedS.

Table 3
Average values of features in the frequency domain for ROEA vs. NoROEA patients.

| Feature      | NoROEA       | ROEA         |
|--------------|--------------|--------------|
| AMSAabs      | 10.994175    | 14.699355    |
| PSA          | 4.529459     | 9.270766     |
| ENRG         | 0.133344     | 0.282428     |
| CF           | 3.763439     | 3.995125     |
| CP           | 0.074070     | 0.167588     |
| DF           | 0.175819     | 0.397635     |
| EF           | 7.447815     | 6.927589     |
| SFM          | 0.027667     | 0.023053     |

Frequency domain features used for description of the frequency characteristics of VF waveforms are:

- amplitude spectrum area (AMSAabs)
- power spectrum analysis (PSA)
- energy (ENRG)
- centroid frequency (CF)
- centroid power (CP)
Fig. 4. Mann–Whitney–Wilcoxon test results on the time-domain features, distinct for the two groups ROEA and NoROEA: a) RMS, b) SA, c) MA, d) WA, e) AmpMax, f) AmpMin, g) PTT, h) PPA i) MS, and j) MedS. P-value annotation legend: ns: $5.00e-02 < p <= 1.00e+00$; *: $1.00e-02 < p <= 5.00e-02$; **: $1.00e-03 < p <= 1.00e-02$; ***: $1.00e-04 < p <= 1.00e-03$; ****: $p < 1.00e-04$.

- dominant frequency (DF)
- edge frequency (EF)
- spectral flatness measure (SFM)

The third group of features computed by the continuous wavelet transform provides concomitant spectral and temporal information:

- total energy in the low-band 1–3 Hz (LBEn)
- total energy in the mid-band 3–10 Hz (MBEn)
- total energy in the high-band 10–32 Hz energy (HBEn)

The fourth group of features indicates the non-linear dynamical nature of VF waveforms:

- standard deviation of the ellipse fitted in the Poincare scatter plot (PSDR)
- area of the ellipse fitted in the Poincare plot (PAREA)
- median stepping increment of the Poincare plot (MSI)
- approximate entropy (ApEn)
Fig. 5. Joint distribution of all pairs of time-domain features.

- shannon entropy (ShEn)
- hurst exponent (H)
- detrended fluctuation analysis (DFA)

As another difference with respect to [3], we make here available the data extracted features computed from the 9s episode immediately prior to the first defibrillation shock on each patient. For preprocessing purpose, each 9s episode was uniformly resampled to 250Hz and band-pass filtered between 0.5–48 Hz to suppress residual baseline drift, power line interference and high frequency noise. The features were then extracted following the definitions given in the references in Table 1.

In Table 2 we show the average values of the features belonging to time domain, for both ROEA and NoROEA outcomes. In Figs. 3 we show the distributions of the time domain features for both ROEA and NoROEA outcomes. The box plots show the min and max values, - outliers excluded -, (upper and lower black lines), the median value (mid black line), and the interquartile range (blue and orange boxes).

In Fig. 4, we show for each time feature, the results of the Mann-Whitney-Wilcoxon test on class separability, while in Fig. 5 we plot the joint distributions of all pairs of features.
Fig. 6. Distribution of samples measured for the frequency-domain, distinct for the two groups ROEA and NoROEA: a) AMSAabs, b) PSA, c) ENRG, d) CF, e) CP, f) DF, g) EF, and h) SFM.

Table 4
Average values of features in the wavelet domain for ROEA vs. NoROEA patients.

| Feature | NoROEA     | ROEA       |
|---------|------------|------------|
| LBEn    | 0.003593   | 0.006895   |
| MBEn    | 0.005152   | 0.009774   |
| HBEn    | 0.004783   | 0.009427   |

Table 5
Average values of features of the non-linear dynamical nature of VF waveforms for ROEA vs. NoROEA patients.

| Feature | NoROEA     | ROEA       |
|---------|------------|------------|
| PSDR    | 8.154644   | 8.034484   |
| PAREA   | 22,836.241321 | 49,338.242941 |
| MSI     | 4.707945   | 7.547057   |
| ApEn    | 0.686185   | 0.709989   |
| ShEn    | 2.086623   | 2.108529   |
| H       | 0.219007   | 0.189328   |
| DFA     | 1.853557   | 1.858302   |

Similarly to what done for time-domain features, Table 3, Figs. 6, 7, and 8 present the same information for frequency features, i.e., the average values of features, the distribution of samples, the Mann–Whitney–Wilcoxon test, and the joint distributions of feature pairs. In Table 4, Figs. 9, 10, and 11 the same data are expressed for wavelet domain features; eventually Table 5, Figs. 12, 13, and 14 replicate the same information for non-linear dynamical features.
2. Experimental Design, Materials and Methods

This database provides the ECG recordings immediately prior to the first countershock in 260 adult patients (>18 yo.) with sudden out-of-hospital cardiac arrest in Brescia, Italy. The data were collected between 2006 and 2009 following the 2005 European CPR guidelines [2]. The ECG data and all relevant demographic information were recorded according to the Utstein guidelines [1] and by using a semiautomatic Heartstart 3000 defibrillator (Laerdal Medical, Stavanger, Norway). The electrodes were placed onto the patients’ torso to comply with a standard lead II configuration. Ethical approval of this study was obtained through the ethical committee of Brescia (application number NP2753).

2.1. ECG original files and ROEA annotations

Patient ECGs recorded during prehospital treatment were first anonymised, then printed in paper, scanned, and finally converted to PDF electronic files. These data contain 9 s of pre-shock and 1 min of post-shock ECGs, for a total length of 9 s and 1 min each. As a difference with respect to the data used in [3], we make here available also the original ECG signals as PDF electronic files.

Three experienced cardiologists were independently examining 1 min post-shock ECGs and annotated each as successful, unsuccessful, or indeterminable. A shock was considered successful if the defibrillation returned organized electrical activity (ROEA) that was confirmed by ECG with...
the heart rate between 40 and 150 beats/min commencing within 1 min post-shock and persisting at least 15 s without continuing CPR. An unsuccessful shock was confirmed if VF, ventricular tachycardia, asystole, low heart rate (<40 beats/min) or pulseless electrical activity occurred after defibrillation.

Based on the cardiologists’ annotations, 9 signals were considered indeterminable and discarded from the analysis. The other 251 valid first shocks were categorized as successful (ROEA) or unsuccessful (NoROEA) based on the majority of doctors’ decisions.
Fig. 10. Mann–Whitney–Wilcoxon test results on the wavelet-domain features, distinct for the two groups ROEA and NoROEA: a) LBEn, b) MBEn, and c) HBEn. P-value annotation legenda: ns: 5.00e-02 < $p$ <= 1.00e+00; *: 1.00e-02 < $p$ <= 5.00e-02; **: 1.00e-03 < $p$ <= 1.00e-02; ***: 1.00e-04 < $p$ <= 1.00e-03; ****: $p$ <= 1.00e-04.

Fig. 11. Joint distribution of pairs of wavelet-domain features.

2.2. Digitized ECG waveforms

The PDF electronic files containing 9 s of pre-shock and 1 min of post-shock ECGs were afterwards digitized by the commercial software FindGraph [5] for storage and offline analysis.
Fig. 12. Distribution of samples measured for the non-linear dynamical nature of VF features, distinct for the two groups ROEA and NoROEA: a) PSDR, b) PAREA, c) MSI, d) ApEn, e) ShEn, f) H, and g) DFA.

Fig. 13. Mann–Whitney–Wilcoxon test results on the non-linear dynamical features, distinct for the two groups ROEA and NoROEA: a) PSDR, b) PAREA, c) MSI, d) ApEn, e) ShEn, f) H, and g) DFA. P-value annotation legenda: ns: 5.00e-02 < p <= 1.00e-00; *: 1.00e-02 < p <= 5.00e-02; **: 1.00e-03 < p <= 1.00e-02; ***: 1.00e-04 < p <= 1.00e-03; ****: p <= 1.00e-04.
Fig. 14. Joint distribution of all pairs of non-linear dynamical features.

Ethics Statement

Ethical approval of this study was obtained through the Ethical Committee of University of Brescia (application number NP2753). In particular, all patients' personal information has been anonymized, and cannot be retrieved starting from the published data.

Declaration of Competing Interest

All authors declare that there is no conflict of interest.

Acknowledgments

The data were collected in the context of the study EC-WAVES, at the University of Brescia (Ethical approval granted by the ethical committee of ASST Spedali Civili Brescia). The data processing was supported partially by European Union’s Horizon 2020 research and innovation programme under the Marie Skłodowska-Curie grant agreement No. 691051 and the Ministry of Education, Science and Technological Development of Serbia (III45010).
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