Discrepancy between true ankle dorsiflexion and gait kinematics and its association with severity of planovalgus foot deformity

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Abstract

Background: In planovalgus deformity with triceps contracture, a midfoot break happens, and ankle dorsiflexion (ADF) occurs at the mid-tarsal joint during gait. Results of standard 3D gait analysis may misinterpret the true ankle dorsiflexion because it recognizes the entire foot as a single rigid segment. We performed this study to investigate whether the severity of planovalgus deformity is associated with the discrepancy between the value of ADF evaluated by physical examination and 3-dimensional (3D) gait analysis. In addition, we aimed to identify the radiographic parameters associated with this discrepancy and their relationships.

Methods: Consecutive 40 patients with 65 limbs (mean age, 11.7 ± 5.5 years) with planovalgus foot deformity and triceps surae contracture were included. All patients underwent 3D gait analysis, and weightbearing anteroposterior (AP) and lateral (LAT) foot radiographs. ADF with knee extension was measured using a goniometer with the patient’s foot in an inverted position.

Results: Twenty-one limbs underwent operation for planovalgus foot deformity, and 56 limbs underwent operation for equinus deformity. The difference between ADF on physical examination and ADF at initial contact on gait analysis was 17.5 ± 8.4°. Differences between ADF on physical examination and ADF at initial contact on gait analysis were significantly associated with the LAT talus-first metatarsal angle (p = 0.008) and calcaneal pitch angle (p = 0.006), but not associated with the AP talus-first metatarsal angle (p = 0.113), talonavicular coverage angle (p = 0.190), talocalcaneal angle (p = 0.946), and naviculocuboid overlap (p = 0.136).

Conclusion: The discrepancy between ADF on physical examination and 3D gait analysis was associated with the severity of planovalgus deformity, which was evaluated on weightbearing LAT foot radiographs. Therefore, physicians should be cautious about interpreting results from 3D gait analysis and perform a careful physical examination to assess the degree of equinus deformity in patients with planovalgus foot deformity.

Keywords: Planovalgus, Ankle dorsiflexion, Physical examination, 3-dimensional gait analysis
Background

Planovalgus deformity is a common foot problem characterized by hind foot valgus, midfoot pronation, decreased medial longitudinal arch, and forefoot abduction/supination [1, 2]. In the flexible type, the medial longitudinal arch is restored performing the Jack and tiptoe tests, and heel alignment is restored when standing on tiptoes. However, the medial arch is not restored in the tiptoe test due to the restricted motion of the subtalar joint in the rigid type, which is often associated with tarsal coalition [3, 4]. Planovalgus is often associated with equinus deformity in patients with cerebral palsy or an idiopathic cause due to contracture of the triceps surae. Most patients are asymptomatic and do not require treatment. However, planovalgus deformity with triceps surae contracture in contrast to simple flexible planovalgus is known to often be symptomatic and cause pain, medial foot callosity, and functional disability [4, 5]. In addition, a previous study using gait analysis showed that increased forefoot abduction occurred throughout the stance phase in symptomatic feet compared to asymptomatic feet [6]. When the deformity becomes symptomatic and conservative treatment fails, operative treatment including calcaneal osteotomy, arthroereisis, talonavicular arthrodesis, and conservative treatment fails, operative treatment including calcaneal osteotomy, arthroereisis, talonavicular fusion, or triple arthrodesis can be considered [2, 4, 7, 8].

Materials and methods

This study was approved by our hospital’s institutional review board, and the need for informed consent was waived because of the retrospective nature of this study.

Study population and data collection

The inclusion criteria were as follows: (1) consecutive patients who visited our hospital for symptomatic planovalgus foot deformity with triceps surae contracture between 2016 and 2018, (2) patients who had weight-bearing anteroposterior (AP) and lateral (LAT) foot radiographs, and (3) patients who underwent 3D gait analysis. The exclusion criteria were as follows: (1) patients who had inadequate foot radiographs for measurements or gait analysis data, (2) patients who had previous surgery for equinus or foot deformity at the time of data collection, and (3) patients who received botulinum toxin injection within 6 months.

From the patients’ medical record review, we collected information regarding patients’ age, sex, etiology, and operative procedures.

Radiographic parameters

Radiographic parameters for assessing the severity of planovalgus deformity were selected based on literature reviews [2, 10–13]. On weightbearing AP foot radiographs, the AP talus-first metatarsal angle (AP talo-1MT) and talonavicular coverage angle (TN) were measured (Fig. 1). AP talo-1MT was defined as the angle between a line drawn through the midpoints of the talar head and neck, and a line bisecting the proximal articular surface of the navicula. On weightbearing LAT foot radiographs, the LAT talus-first metatarsal angle (LAT talo-1MT), calcaneal pitch angle (CP), LAT talocalcaneal angle (TC), and naviculocuboid (NC) overlap were measured (Fig. 2). LAT talo-1MT was defined as the angle between a line bisecting the long axis of the first metatarsal bone and a line drawn through the midpoints of the talar head and neck. CP was defined as the angle between a line drawn along the edge of the plantar soft tissue shadow and a line drawn along the lower margin of the calcaneus. TC was defined as the angle between a line drawn through the midpoints of the talar head and neck, and a line drawn along the lower margin of the calcaneus. NC overlap was defined as the overlapping portion of the navicula and cuboid divided by the vertical height of the cuboid.

Radiographic measurements were performed using picture archiving and communication software (INFINITT Healthcare, Seoul, Korea). Before the main measurements were determined, the inter-observer reliability
of the radiographic measurements of 15 AP and LAT standing foot radiographs was tested by two orthopedic surgeons (KBK and JHL). Thereafter, radiographic measurements for all patients were determined by one author (JHL).

Gait analysis
All patients underwent 3D gait analysis using a Motion Analysis system (Motion Analysis Corporation, CA, USA) that was equipped with 10 cameras and two force plates. Markers were placed by two operators according to the Helen Hayes marker set. Nineteen markers were used in the static trials, and 15 lower body markers were used in the dynamic walking trials [14]. Patients walked barefoot on a 9-m walkway over three times at an interval of approximately 30 s, and kinematic data and temporal parameters were recorded. Three trials representing patients' typical gait pattern were selected and averaged. Sagittal kinematics of the ankle joint including ankle dorsiflexion at initial contact, mean ankle dorsiflexion in the stance phase, and peak ankle dorsiflexion in the stance phase were considered as outcome variables.

Physical examination
Physical examinations were performed by pediatric orthopedic fellows, before 3D gait analysis, and a goniometer was used to assess range of motions of the hip, knee, and ankle joints. For the ankle joint, one arm of the goniometer was placed along a bisection of the LAT aspect of the lower leg, and the other arm was placed along the LAT margin of the hindfoot. When measuring ADF, the foot was inverted to lock the mid-tarsal joint and to avoid dorsiflexion at the mid-tarsal joint. ADF with knee extension was considered as an outcome variable.

Statistical analysis
Intraclass correlation coefficients (ICCs) and 95% confidence intervals were used to assess interobserver reliabilities for radiographic measurements. ICCs were calculated in the setting of a two-way random effect model, assuming a single measurement and absolute agreement [15]. ICC values > 0.8 indicate excellent reliabilities.

Descriptive statistics, such as means and standard deviations, were used to summarize the data. To consider the inclusion of bilateral limbs, a linear mixed model was used to estimate the discrepancy between ADF on physical examination and 3D gait analysis with radiographic parameters [16].

Statistical analyses were performed using SAS 9.4 (SAS Institute, Cary, NC, USA) and SPSS software for Windows (version 25.0; IBM Corp., Armonk, NY, USA). All statistics were two-tailed, and a p-value < 0.05 was considered significant.

Results
Forty-four patients with 73 limbs were initially identified in our database. After applying the exclusion criteria, 40 patients with 65 limbs were finally included in this study. Etiologies were cerebral palsy in 33 patients and idiopathic in 7 patients. Mean patients' age at the time of evaluation was 11.7 years (median, 9.5; range, 5.2–25.3) and 35 patients were under 18 years old. Bilateral feet were included in 25 patients and unilateral foot in 15 patients. No patients showed arthritic change of the ankle joint. Among the 40 patients, 36 patients with

Fig. 1 On weightbearing anteroposterior (AP) foot radiographs, the AP talus-first metatarsal angle (AP t1-MT) and talonavicular coverage angle (TN) are measured.
58 limbs underwent surgeries. The total number of surgical procedures was 158 (2.7 per limbs). Twenty-one limbs underwent operation for planovalgus foot deformity (calcaneal lengthening, 20; talonavicular fusion, 1), and 56 limbs underwent operation for equinus deformity (Table 1).

Radiographic measurements had excellent interobserver reliabilities for all radiographic parameters (ICC, 0.860–0.985) (Table 2). On physical examination, ankle dorsiflexion in knee extension was $-20.6 \pm 11.3^\circ$. On sagittal kinematics of gait analysis, ADF at initial contact, mean ADF in the stance phase and peak ADF in the stance phase were $-3.2 \pm 7.0^\circ$, $5.2 \pm 7.5^\circ$ and $11.3 \pm 8.5^\circ$, respectively (Table 3). The difference between ADF on physical examination and ADF at initial contact on gait analysis was $17.5 \pm 8.4^\circ$.

Differences between the ADF on physical examination and the ADF at initial contact on gait analysis were significantly associated with LAT talo-1MT ($p=0.008$) and CP ($p=0.006$) (Fig. 3a and b), but not with AP talo-1MT ($p=0.113$), TN ($p=0.190$), TC ($p=0.946$), and NC overlap ($p=0.136$). Similar findings were found in terms of differences between ADF on physical examination and mean ADF in the stance phase, and between ADF on physical examination and peak ADF in the stance phase (Table 4).

**Discussion**

We demonstrated that the discrepancy between ADF assessed by physical examination and 3D gait analysis is significantly associated with two radiographic parameters on weight-bearing LAT foot radiographs: LAT talo-1MT and CP. This finding supports our hypothesis that the discrepancy between ADF on physical examination and 3D gait analysis is associated with the severity of planovalgus deformity.

ADF is essential for the forward translation of the center of gravity of the body during the second rockers of the gait cycle [17]. If the ADF is restricted due to the contracture of the triceps surae, ADF occurs at the midtarsal joint, and this may eventually lead to midfoot breakage and planovalgus foot deformity. For patients with planovalgus deformity, it is essential to evaluate the

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**Table 1** Patient demographics and summary of operative procedures

| Parameters                      | Values                      |
|---------------------------------|-----------------------------|
| Sex (male / female)             | 29 / 11                     |
| Age (years)                     | $11.7 \pm 5.5$ (range: 5.2–25.3) |
| Side (right / left)             | 35 / 30                     |
| Etiology (Cerebral palsy / Idiopathic) | 33 / 7                  |
| Operative procedures Number of limbs |                            |
| Calcaneal lengthening           | 20                          |
| Talonavicular fusion            | 1                           |
| Intramuscular psoas lengthening | 5                           |
| Adductor tenotomy               | 2                           |
| Dega pelvic osteotomy           | 2                           |
| Femoral derotaton osteotomy     | 7                           |
| Femoral varization osteotomy    | 2                           |
| Distal hamstring lengthening    | 32                          |
| Rectus femoris transfer         | 27                          |
| Tendo-Achilles lengthening or Strayer procedure | 56                  |
| Tibial derotation osteotomy     | 2                           |
| Kidner operation                | 2                           |
Table 2 Inter-observer reliabilities of radiographic measurements

| Radiographic parameter                  | Inter-observer reliability | ICC    | 95% CI       |
|----------------------------------------|----------------------------|--------|--------------|
| AP talus-1st metatarsal angle (°)       |                            | 0.976  | 0.930–0.992 |
| Talonavicular coverage angle (°)       |                            | 0.876  | 0.549–0.961 |
| Lateral talus-1st metatarsal angle (°)  |                            | 0.969  | 0.908–0.990 |
| Calcaneal pitch angle (°)              |                            | 0.985  | 0.954–0.995 |
| Talocalcaneal angle (°)                |                            | 0.918  | 0.779–0.971 |
| Naviculocuboid overlap (%)             |                            | 0.981  | 0.945–0.994 |

ICC intraclass correlation coefficient, CI confidence interval

A degree of ADF in order to determine appropriate treatment methods.

In the standard 3D gait analysis, the rigid single-segment foot model is based on a vector that passes from the calcaneus to the space between the 2nd and the 3rd metatarsal. The motion of this foot vector relative to the plantar surface represents the ankle plantarfexion and dorsiflexion [18]. When the patient presents with a mid-foot breakage, this marker placement can result in the exaggeration of ADF. In other words, an insufficient amount of ADF is compensated by midfoot breakage in a planovalgus deformity [9]. To avoid or reduce this measurement artifact, a toe marker can be placed more proximally toward the midfoot by the clinician or the operators in gait lab [19]. However, this toe marker adjustment was not made in this study due to its retrospective design.

To overcome the disadvantage of standard 3D gait analysis, 3D multi-segment foot models, such as the DuPont foot model, Oxford foot model, Milwaukee foot model, Leardini foot model, and Heidelberg foot model, have been increasingly used because they can illustrate the effect of foot and ankle pathologies on intersegmental motion of the foot [20–27]. However, repeatability of the multi-segment foot model is lower in the pediatric population than in the adult population because it is difficult to attach the marker to the correct position in small feet [28, 29]. Thus, use of the 3D multi-segment foot model might be limited in pediatric patients. Therefore, a careful physical examination should be performed to assess ankle range of motion in planovalgus deformity. The subtalar joint must be inverted to the neutral position and locked in that position in order to isolate and evaluate the dorsiflexion at the ankle joint, not the mid-tarsal joint.

We think that there may be a discrepancy between true ADF on physical examination and ADF on gait analysis, and that the severity of planovalgus deformity may be associated with this discrepancy. The severity of planovalgus deformity can be evaluated on weight-bearing AP and LAT foot radiographs. Previous studies showed that AP talo-1MT, TN, NC overlap and LAT talo-1MT were valid and reliable radiographic indices for evaluating planovalgus foot deformity [2, 11]. This study also showed that these radiographic indices had excellent interobserver reliabilities for measurements indicating their relevance for clinical use. Other radiographic parameters including Kite’s angle, Costa-Bertani’s angle, and the talar declination angle also can be used to evaluate planovalgus deformity [30]. In this study, only two radiographic parameters including LAT talo-1MT and CP, which were measured on LAT radiographs, were associated with the discrepancy between ADF on physical examination and 3D gait analysis. However, radiographic parameters on AP radiographs including AP talo-1MT and TN were not associated with this discrepancy. LAT talo-1MT is the angle between the longitudinal axis of the first metatarsal bone and talus on a LAT weightbearing foot radiograph. Increased LAT talo-1MT indicates a more vertically positioned talus, which represents increased midfoot breakage and increased dorsiflexion at the mid-tarsal joint. CP represents the relative position of the calcaneus to the ground, and decreased CP means increased dorsiflexion at the mid-tarsal joint. Our finding that increased LAT talo-1MT and decreased CP were associated with the discrepancy between ADF on physical examination and 3D gait analysis is reasonable. Therefore, clinicians should consider LAT talo-1MT and CP to assess ADF from 3D gait analysis in patients with planovalgus deformity.

Contracture of the triceps surae lead to midfoot breakage and planovalgus foot deformity. Correction of the equinus deformity by tendo-Achilles lengthening might help ameliorate planovalgus deformity as improvement in dorsiflexion of the ankle joint results in the improvement of midfoot breakage. Further study regarding the changes in bony alignment of the foot after tendo-Achilles lengthening for planovalgus deformity is required.

Table 3 Summary of radiographic measurements, physical examination and sagittal kinematics of ankle joint

| Radiographic parameter                  | Mean ± SD  | Range          |
|----------------------------------------|------------|----------------|
| AP talus-1st metatarsal angle (°)       | 23.5 ± 13.7| 0.7 to 73.4    |
| Talonavicular coverage angle (°)       | 32.3 ± 12.3| 8.5 to 61.9    |
| Lateral talus-1st metatarsal angle (°)  | 33.9 ± 15.1| 8.1 to 76.8    |
| Calcaneal pitch angle (°)              | 8.9 ± 7.6  | −14.4 to 21.7  |
| Talocalcaneal angle (°)                | 56.1 ± 9.1 | 30.9 to 77.3   |
| Naviculocuboid overlap (%)             | 75.6 ± 19.2| 13.0 to 100    |
| Physical examination                   |            |                |
| Ankle dorsiflexion in knee extension (°)| −20.6 ± 11.3| −50.0 to −5.0 |
| Sagittal kinematics of ankle joint     |            |                |
| Ankle dorsiflexion at initial contact (°)| −3.2 ± 7.0  | −36.5 to 8.7   |
| Mean ankle dorsiflexion in stance (°)  | 5.2 ± 7.5  | −37.7 to 19.4  |
| Peak ankle dorsiflexion in stance (°)  | 11.3 ± 8.5 | −32.8 to 29.8  |
There are limitations to this study. First, we used a goniometer to measure ADF despite lower reported reliability values with use of this device. Several authors introduced various valid and reliable devices for measuring ADF [31–33]. However, other devices could not measure ADF with the foot in an inverted position. In addition, the goniometer is commonly used in the clinical setting, and ADF was measured using a uniform protocol in this study. Therefore, we think that our results may be clinically meaningful. Second, our results may not be generalized to all patients with planovalgus deformities and triceps surae contractures, because most of our study subjects were children and adolescents. Therefore, further study on an adult cohort is required. Third, ADF with knee extension was considered an outcome variable in this study. Use of ADF with knee flexion might change the results. However, the results regarding ADF with knee flexion are absent due to the retrospective

| Parameter                                | Estimate | SE    | p-value | Estimate | SE    | p-value | Estimate | SE    | p-value |
|------------------------------------------|----------|-------|---------|----------|-------|---------|----------|-------|---------|
| AP talus-1st metatarsal angle            | -0.13    | 0.08  | 0.113   | -0.12    | 0.09  | 0.203   | -0.10    | 0.10  | 0.353   |
| Talonavicular coverage angle             | -0.14    | 0.08  | 0.190   | -0.193   | 0.09  | 0.052   | -0.19    | 0.10  | 0.068   |
| Lateral talus-1st metatarsal angle       | -0.19    | 0.07  | 0.008   | -0.22    | 0.08  | 0.010   | -0.23    | 0.08  | 0.011   |
| Calcaneal pitch angle                    | 0.42     | 0.14  | 0.006   | 0.41     | 0.17  | 0.023   | 0.44     | 0.18  | 0.023   |
| Talocalcaneal angle                      | 0.01     | 0.11  | 0.946   | -0.01    | 0.13  | 0.917   | -0.03    | 0.14  | 0.837   |
| Naviculocuboid overlap                   | 8.47     | 5.49  | 0.136   | 8.56     | 6.41  | 0.195   | 8.63     | 6.86  | 0.220   |

ADF ankle dorsiflexion
design of this study. Therefore, further prospective research including ADF with both knee extension and knee flexion is needed.

Conclusions
The discrepancy between ADF on physical examination and 3D gait analysis was associated with the severity of planovalgus deformity, which was evaluated on weight-bearing LAT foot radiographs. Therefore, physicians should be cautious about interpreting results from 3D gait analysis and perform a careful physical examination to assess the degree of equinus deformity in patients with planovalgus foot deformity. Further research is required to develop and validate sophisticated foot marker placements when performing standard 3D gait analysis in patients with foot deformity.

Abbreviations
3D: 3-dimensional; ADF: Ankle dorsiflexion; AP: Anteroposterior; LAT: Lateral; talo-1MT: Talus-first metatarsal angle; TN: Talonavicular coverage angle; CP: Calcaneal pitch angle; TC: Lateral talocalcaneal angle; NC: Naviculocuboid; ICC: Intraclass correlation coefficient

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Authors’ contributions
CYC and MSP participated in the design of this study. KHS, KBK and JHL participated in data acquisition and collection. KHS, CYC and KML analyzed the data. KHS and MSP drafted the manuscript. KHS and KBK performed the statistical analysis. All authors read and approved the final manuscript.

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Availability of data and materials
The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

Ethics approval and consent to participate
This retrospective study was approved by the institutional review board of our hospital (B-1906-547--104), and informed consent was waived owing to the retrospective nature of the study.

Consent for publication
Not applicable.

Competing interests
The authors declare that they have no competing interests.

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References
1. Adams SB Jr, Simpson AW, Pugh LJ, Stasikelsis PJ. Calcaneocuboid joint subluxation after calcaneal lengthening for planovalgus foot deformity in children with cerebral palsy. J Pediatr Orthop. 2009;29(2):170–4.
2. Sung KH, Chung CY, Lee KM, Lee SY, Park MS. Calcaneal lengthening for planovalgus foot deformity in patients with cerebral palsy. Clin Orthop Relat Res. 2013;471(5):1682–90.
3. Pavone V, Vescio A, Di Silvistea CA, Andreacchio A, Sessa G, Testa G. Outcomes of the calcaneo-stop procedure for the treatment of juvenile flatfoot in young athletes. J Child Orthop. 2018;12(6):582–9.
4. Mosca V. Flexible flatfoot in children and adolescents. J Child Orthop. 2010;4(2):107–21.
5. Pavone V, Vescio A, Canavesi F, Costa D, Sessa G, Testa G. Effects of body weight on the clinical and radiological outcomes of children with flexible flatfoot managed with the ‘calcaneo-stop’ procedure. J Pediatr Orthop B. 2019;28(3):228–34.
6. Kerr CM, Zavatsky AB, Theologis T, Stebbins J. Kinematic differences between neutral and flat feet with and without symptoms as measured by the Oxford foot model. Gait Posture. 2019;67:213–8.
7. Bauer K, Mosca VS, Zions LE. What’s new in pediatric flatfoot? J Pediatr Orthop. 2016;36(8):865–9.
8. Mosca V. Calcaneal lengthening for valgus deformity of the hindfoot. Results in children who had severe, symptomatic flatfoot and skewfoot. J Bone Joint Surg Am. 1995;77(4):500–12.
9. Kim HY, Shin HS, Ko JH, Cha YH, Ahn JH, Hwang JY. Gait analysis of symptomatic flatfoot in children: an observational study. Clin Orthop Surg. 2017;9(3):363–73.
10. Sung KH, Kwon SS, Chung CY, Lee KM, Park MS. Radiographic changes of the mid-tarsal joint after calcaneal lengthening for planovalgus foot deformity. Foot Ankle Surg. 2020;26(1):110–15.
11. Lee KM, Chung CY, Park MS, Lee SH, Cho JH, Choi IH. Reliability and validity of radiographic measurements in hindfoot varus and valgus. J Bone Joint Surg Am. 2010;92(13):2319–27.
12. Westberry DE, Davids JR, Roush TF, Pugh LJ. Qualitative versus quantitative radiographic analysis of foot deformities in children with hemiplegic cerebral palsy. J Pediatr Orthop. 2008;28(3):359–65.
13. Davids JR, Gibson TW, Pugh LJ. Quantitative segmental analysis of weight-bearing radiographs of the foot and ankle for children: normal alignment. J Pediatr Orthop. 2005;25(6):769–76.
14. Sung KH, Chung CY, Lee KM, Akhmedov B, Lee SY, Choi IH, Choi TJ, Yoo WJ, Park MS. Long term outcome of single event multilevel surgery in spastic diplegia with flexed knee gait. Gait Posture. 2013;37(4):536–41.
15. Lee KM, Lee J, Chung CY, Ahn S, Sung KH, Kim TW, Lee HJ, Park MS. Pitfalls and important issues in testing reliability using intraclass correlation coefficients in orthopaedic research. Clin Orthop Surg. 2012;4(2):149–55.
16. Park MS, Kim SJ, Chung CY, Choi IH, Lee SH, Lee KM. Statistical consideration for bilateral cases in orthopaedic research. J Bone Joint Surg Am. 2010;92(8):1732–7.
17. Dananberg HJ. Manipulation of the ankle as a method of treatment for ankle and foot pain. J Am Podiatr Med Assoc. 2000;94(4):395–9.
18. Kadaba MP, Ramakrishnan HK, Wootten ME. Measurement of lower extremity kinematics during level walking. J Orthop Res. 1990;8(3):383–92.
19. Harris GF, Smith PA. Foot and ankle motion analysis: clinical treatment and technology. 1st ed. Boca Raton: CRC Press; 2007.
20. Caravaggi P, Benedetti MG, Berti L, Leardini A. Repeatability of a multi-segment foot model with a 15-marker set in healthy adults. J Foot Ankle Res. 2014;7:24.
21. Wright CJ, Arnold BL, Coffey TG, Pidcoe PE. Repeatability of the modified Heidelberg foot measurement method: development, description and assessment. Gait Posture. 2010;31(1):32–6.
22. Kim EJ, Shin HS, Lee JH, Kyung MG, Yoo HJ, Yoo WJ, Lee DY. Repeatability of a multi-segment foot model with a 15-marker set in Normal children. Clin Orthop Surg. 2018;10(4):484–90.
23. Long JT, Eastwood DC, Graf AR, Smith PA, Harris GF. Repeatability and sources of variability in multi-center assessment of segmental foot kinematics in normal adults. Gait Posture. 2010;31(1):32–6.
24. McCahill J, Stebbins J, Koning B, Harlaar J, Theologis T. Repeatability of the Oxford foot model in children with foot deformity. Gait Posture. 2018;61:86–9.
25. Seo SG, Lee DY, Moon HJ, Kim SJ, Kim J, Lee KM, Chung CY, Choi IH. Repeatability of a multi-segment foot model with a 15-marker set in healthy adults. J Foot Ankle Res. 2014;7:24.
26. Simon J, Doederelin L, McIntosh AS, Metaxiotis D, Bock HG, Wolf SL. The Heidelberg foot measurement method: development, description and assessment. Gait Posture. 2006;23(4):411–24.
27. Wright CJ, Arnold BL, Coffey TG, Pidcoe PE. Repeatability of the modified Oxford foot model during gait in healthy adults. Gait Posture. 2011;33(1):108–12.
28. Saraswat P, MacWilliams BA, Davis RB, D’Astous JL. A multi-segment foot model based on anatomically registered technical coordinate systems: method repeatability and sensitivity in pediatric planovalgus feet. Gait Posture. 2013;37(1):121–5.
28. Stolze H, Kuhtz-Buschbeck JP, Mondwurf C, Johnk K, Friege L. Retest reliability of spatiotemporal gait parameters in children and adults. Gait Posture. 1998;7(2):125–30.
29. Stebbins J, Harrington M, Thompson N, Zavatsky A, Theologis T. Repeatability of a model for measuring multi-segment foot kinematics in children. Gait Posture. 2006;23(4):401–10.
30. Pavone V, Costarella L, Testa G, Conte G, Riccioli M, Sessa G. Calcaneo-stop procedure in the treatment of the juvenile symptomatic flatfoot. J Foot Ankle Surg. 2013;52(4):444–7.
31. Jung KS, Yu JY, Kim SY, Lee DK, Oh JS. Reliability of ankle dorsiflexion passive range of motion measurements obtained using a hand-held goniometer and Biodex dynamometer in stroke patients. J Phys Ther Sci. 2015;27(6):1899–901.
32. Calatayud J, Martin F, Gargallo P, Garcia-Redondo J, Colado JC, Marin PJ. The validity and reliability of a new instrumented device for measuring ankle dorsiflexion range of motion. Int J Sports Phys Ther. 2015;10(2):197–202.
33. Gatt A, Chockalingam N. Validity and reliability of a new ankle dorsiflexion measurement device. Prosthetics Orthot Int. 2013;37(4):289–97.

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