Review Article

Current Perspectives on In Vivo Noninvasive Tracking of Extracellular Vesicles with Molecular Imaging

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Clinical and preclinical in vivo tracking of extracellular vesicles (EVs) are a crucial tool for the development and optimization of EV-based diagnosis and treatment. EVs have gained interest due to their unique properties that make them excellent candidates for biological applications. Noninvasive in vivo EV tracking has allowed marked progress towards elucidating the mechanisms and functions of EVs in real time in preclinical and clinical studies. In this review, we summarize several molecular imaging methods that deal with EVs derived from different cells, which have allowed investigations of EV biodistribution, as well as their tracking, delivery, and tumor targeting, to determine their physiological functions and to exploit imaging-derived information for EV-based theranostics.

1. Introduction

The naturally produced biological nanoparticles, termed extracellular vesicles (EVs), are released from most of cells into the extracellular space. These include exosomes (40–100-nm diameter membranous vesicles of endocytic origin) and microvesicles (large membranous vesicles of 50–500-nm diameter), which are shed directly from the plasma membrane [1, 2]. Proteins and lipids are the main components of EV membranes, which are enriched with lipid rafts [3]. EVs are capable of carrying various biological materials such as lipids, proteins, mRNA, and miRNA [3–6]. A previous study has also demonstrated that pancreatic cancer cell-derived EVs can contain fragments of double-stranded genomic DNA [7]. Intercellular communication is essential to cell development and maintenance of homeostasis in multicellular organisms. These communications between cells can be localized or distant. Distant intercellular communication in particular is achieved via EVs [8, 9]. A major discovery has been that the cargo of EVs included both mRNA and miRNA; mRNAs could be translated into proteins in target cells [6, 10].

The recent studies showed that the biological roles of EVs ranged from normal physiological functions, such as stem cells in kidney monitoring and repair [11, 12], immune modulation [13], and tissue homeostasis [14], to contributing to the pathophysiology of several diseases [10]. EVs can modulate immune-functional properties against tumors and set up tumor escape mechanisms [15]. EVs are ideal vehicles for molecule-delivery (suicidal proteins and RNAs, small molecule drugs, etc.) to certain cells, because of their biocompatibility, stability in blood circulation, and, most importantly, their ability to target certain cell types [16]. Even though the first discovery of EV’s role in cell-cell communication was made in the 1990s [17], more discoveries continue to be made. During the past few years, there has been enormous progress in our understanding of the function of EVs and their possible applications in clinical settings [18], yet more biological roles remain to be discovered. The role of EVs in vivo communication and their applicability as vehicles for drug-delivery to targets require the investigation of their biodistribution.

Noninvasive imaging modalities have the potential of providing better understanding of the biological process and effectiveness of EVs for various diseases by determining the in vivo kinetics of EVs. Molecular imaging are mainly categorized into two main technique classes, namely, direct and indirect labeling. Direct labeling involves labeling of EVs by means of various agents, such as magnetic particles [19],
lipophilic tracer dyes [20], or radionuclides [21], while, in indirect labeling, cells are genetically altered to transcribe and translate reporter proteins, and the EVs containing the reporter proteins are then isolated [22, 23].

Here, we will review studies that used molecular imaging techniques to evaluate EV visualization, biodistribution, and targeted drug-delivery in certain diseases and further discuss important issues in this area. We also provide a general overview and specific examples of in vivo tracking of EVs by means of various imaging modalities, to enhance understanding of the roles of EVs in various pathophysiological conditions.

2. Biogenesis of Extracellular Vesicles

EVs are secreted from various cells, such as immune cells (T and B cells, dendritic cells, natural killer cells, monocytes/macrophages, platelets, and red blood cells [RBCs]) [24–29]; mesenchymal stem cells (MSCs) [14]; and tumor cells (glioblastoma, thyroid, lung, breast, liver, ovarian, and colon cancers) [30–35]. Bacteria and plants also secrete EVs [36, 37]. Even though almost all cells are able to release EVs with various biological and pathological functions, they were considered as "garbage bags" in the past.

2.1. Exosomes. Endocytic membrane trafficking is controlled through several cytosolic regulatory mechanisms that dictate the number, composition, and fate of vesicles in their lumen (i.e., intraluminal vesicles, ILVs) and exosomes [44, 45]. Multivesicular bodies (MVBs) (Figure 1(a)), which appear along the endocytic pathway, are characterized by the presence of ILVs formed by inward budding of the outer cell membrane [46]. Exosome biogenesis and cargo sorting involves the coordinated recruitment and employment of endosomal sorting complex required for transport (ESCRT) machinery and its associated proteins [47–49]. A study by Ostrowski et al. established that a number of Rab family proteins (including Rab27a and Rab27b) act as vital regulators of exosome release [50]. However, the mechanism behind this process is not yet completely understood.

2.2. Microvesicles. The small vesicles are shed from the surface of many cells called microvesicles (Figure 1(a)) [51]. Microvesicles are slightly larger than exosomes and can therefore carry more cargo load than exosomes. EVs (exosomes and microvesicles) can be identified under electron microscopy by their round shape and the presence of a lipid bilayer (Figure 1(b)).

3. Emerging Therapeutic and Diagnostic Potential of Extracellular Vesicles

Recent studies have revealed the biopathological roles of EVs in treatment, drug-delivery, tumor progression, and disease diagnosis [52]. Recently, the therapeutic application of EVs has also emerged [53]; for example, the application of dendritic cell- (DC-) derived exosomes for cancer treatment was recently investigated in a clinical trial (NCT01159288) [54, 55]. MSC-EVs have been proposed as a replacement for MSCs for the treatment of various diseases, such as for tumor inhibition and cardiac and brain injuries [56–60]. MSC-derived exosome for Crohn's fistula treatment was recently under investigation in a clinical trial [61, 62].

The emerging evidence that EVs possess special characteristics may indicate that they can be used to create an EV-based drug-delivery system that is superior to synthetic drug carriers [53]. A previous study used exosomes for delivering curcumin as a treatment for an inflammatory disease [63]. To enhance the function of drugs in the central nervous system, exosomes can also carry small molecular drugs across the blood-brain barrier [64].

Tumor-derived EVs may enhance tumor cell activity. For example, exosomes released from breast carcinomas stimulate cancer cell movement, leading to establishment of distant metastasis [65]. Recent studies showed that tumor-derived
EVs promote endothelial cell migration during angiogenesis in the tumor microenvironment via ERK1/2 and JNK signaling pathways [66]. Numerous studies have shown that tumor-derived EVs transfer oncogenic activity, thus promoting tumor progression [67, 68]. Tumor-secreted exosomes have been shown to facilitate tumor progression by affecting the adhesion of the primary cancer cells and promoting metastasis [65, 69].

Recently, other biomarker-like exosomes have been investigated. Glypican-1 and endothelial locus-1 positive exosomes may serve as potential noninvasive diagnostic tools for detecting the early stages of pancreatic cancer and breast cancer, respectively [70, 71]. Multiple research groups are actively seeking novel biomarkers, including EV-based markers, for detecting hidden cancers at the earliest possible stage.

4. Molecular Imaging Techniques for Tracking Extracellular Vesicles

Methods that allow EV monitoring in vivo offer several advantages over the traditional ex vivo methods, which require sacrifice of the animal and histological analysis. Molecular imaging, for example, is fundamentally noninvasive and allows for quantitative assessment of the EV biodistribution and the effects of EV therapy over time (Figure 2). Bioluminescent imaging (BLI) and fluorescence imaging (FLI) have the advantage of high-throughput efficiency at low cost.

BLI uses light generated from a luciferase enzyme-substrate and an ultraviolet cooled charge-coupled camera for signal detection. In indirect labeling of EVs, the cells are first transfected with a vector containing imaging reporter genes (e.g., Gaussia luciferase [Gluc]). These cells then produce Gluc mRNA which is translated into the reporter protein. Isolation of EVs from these cells will provide EVs containing the reporter protein from the cell. In stably transfected cells, the reporter gene is inherited by daughter cells upon cell division. This strategy is essential for long-term isolation of EVs containing the reporter protein.

FLI signal generation is achieved by exciting the fluorescent proteins/dye at a given light wavelength and detection of the light emission at another wavelength by means of a charge-coupled camera. In indirect labeling of EVs with a fluorescent protein (GFP/RFP) [23, 72], the same method is used as that for bioluminescent reporter proteins. Direct labeling of EVs with a fluorescent dye is a very simple technique to perform. EVs can be washed a few times after incubation with a fluorescent lipophilic dye [12, 73, 74], and they are then ready for in vivo experiments. Direct labeling of EVs with fluorescent dyes has a few drawbacks. The exogenous dye labeling produces a nonspecific signal due to the long half-life of the fluorescent dye and its resistance to degradation. One of the main considerations when a fluorescent dye is used to label the membranes of the EVs is that the dye can be released from the EVs; this can lead to generation of non-EV-associated signals [74–76]. Compared to BLI, FLI is generally less sensitive, due to the higher background signal. In most cases, FLI is used for live imaging of shallow tissue areas.

Nuclear imaging is also a widely used molecular imaging technique. As radionuclides emit gamma rays or positrons,
radionuclides can be detected, even when located deep in organs. Radionuclides can be placed inside EVs [20, 21] or be incorporated as a label in membrane proteins of EVs [41, 42].

Magnetic resonance imaging (MRI) can be used for tracking EVs after labeling with ultrasmall superparamagnetic iron oxide nanoparticles (USPIO, 4–6 nm) [20, 43]. As MRI provides high-resolution anatomical images, we can easily discriminate the location of the EVs. However, it is limited by its relatively lower sensitivity of detection than that of other molecular imaging modalities [77].

5. Tracking Extracellular Vesicles by Bioluminescence Imaging

BLI is a powerful method for cell tracking in small animals (such as mice) over time, without requiring the subject to be euthanized [78–80]. Bioluminescence reporters are able to reveal the in vivo biodistribution and allow tracking of EVs with very high sensitivity. To date, there have been very few studies that have used bioluminescence reporters for in vivo visualization and tracking of the distribution of EVs (Table 1) [22, 23, 38].

5.1. Direct Labeling Methods. To date, there has been no report about direct bioluminescence reporter-based labeling of EVs. Yet, it is possible to achieve labeling of EVs with bioluminescence reporters. A few other studies have shown that exogenous peptide, proteins, and siRNA can be loaded into EVs [81–83]; similarly, it is possible to load exogenous bioluminescence reporter proteins into EVs, which could be used for visualizing and monitoring EVs in vivo in the near future.

5.2. Indirect Labeling Methods. Gluc is a reporter protein that emits bioluminescence when its substrate, coelenterazine, is present, and lactadherin is a membrane-associated protein mainly found in exosomes. This is referred to as Gluc-lactadherin which is eventually found in the exosomes [23]. A previous study used melanoma cell (B16-BL6) to produce exosomes, in which they transfected cells with a Gluc-lactadherin construct. Intravenous injection of these exosomes revealed for the first time that EVs could be visualized in vivo by using bioluminescent reporter proteins present in exosomes. This study provided the overall tissue distribution and quantitative pharmacokinetic properties of exosomes in vivo and proved that exosomes have very short half-lives after systemic administration. This was not possible with dye-based EV studies, as dye can be released from the EVs, which can lead to non-EV-associated signals [23].

In another study, Gluc was fused to a biotin acceptor domain in cells, which then produced the labeled EVs. Intravenous injection of EVs derived from these cells revealed that the EVs could be visualized in vivo and showed an organ-specific distribution of EVs. The Gluc signal was observed in the spleen and liver in the EV-injected mice and later in the liver and kidney of these mice. This was eventually quantified by determining the average bioluminescent radiance in organ regions of the mice. The advantage of this study was that it combined both Gluc and biotin to create an EV-specific reporter with a high sensitivity for studying in vivo dynamics of systemically administered EVs. The BLI revealed that most EV-Gluc was cleared from the animals by 6 h after injection and also showed that EVs could be targeted to tumors [22].

Another study also used Gluc-lactadherin for exosome labeling. It clearly indicated that macrophages play a major role in the clearance of exosomes in general, by using BLI [38]. All three studies showed rapid in vivo distribution of EVs in animals.

6. Tracking Extracellular Vesicles by Optical Fluorescence

The strategy for imaging and tracking for EVs by labeling them fluorescently has been widely used to investigate in vivo behavior of exogenous EVs both in vitro and in vivo (Table 1) [12, 20, 39, 40, 72, 84–86].

6.1. Direct Labeling Methods. The direct labeling protocol is very simple and there is no need to use genetically modified EVs (Figure 3). This simple imaging strategy, which uses dye to label the lipid membrane of EVs, has been used to reveal the spatiotemporal location of systemically injected exogenous EVs in organs and target tumors [12, 40]. Grange et al. have demonstrated that it is possible to analyze the biodistribution of EVs by direct labeling of EVs with a DiD dye. In particular, they observed that the labeled MSC-derived EVs were localized within injured kidneys in vivo. The signal generated by the EVs was maintained even 24 h after the injection [12].

Hood et al., using a lipophilic tracer dye (DiD), showed that the melanoma exosome prepares the way for metastasis of this cancer to the sentinel lymph nodes [84]. Another study used DiR labeling of EVs to show delivery of Let-7a miRNA by exosomes to epidermal growth factor receptor-expressing breast cancer cells in vivo, which was confirmed ex vivo [40]. Smyth et al. compared the biodistribution and delivery efficiency of tumor-derived exosomes and liposomes by using a lipophilic dye (DiR). FLI revealed that tumor-derived exosomes and liposomes had a similar clearance time in vivo. Furthermore, this study also revealed that liposomes and tumor-derived exosomes were not targeted to the tumor when injected systematically. Moreover, FLI showed that tumor-derived exosomes and liposomes injected into the tumor stayed within the tumor [20].

Wiklander et al. used a near-infrared dye (DiR) and studied the biodistribution profile of EVs derived from a broad range of different cell types, namely, HEK293T, primary mouse DCs, and primary human MSCs. DiR-labeled HEK293T EVs were subsequently injected via the tail vein of mice, but the fluorescent signal in whole mouse imaging did not yield sufficient accuracy to determine from which tissue or organ the signal originated; thus, organs were harvested and imaged ex vivo. They also showed that different routes of injection (intravenous, intraperitoneal, and intramuscular) yielded different distribution patterns for EV signals from organs and tissues. Furthermore, FLI revealed that distributions of EVs derived from different cells yielded different distribution patterns in internal organs. They also
## Table 1: Strategies of in vivo tracking of extracellular vesicles.

| Imaging modality | Labeling strategy | Types of cells | Isolation method | Labeling method | Injection Site | Subject | Duration of tracking | Purpose | Clinical translation | Reference |
|------------------|-------------------|----------------|------------------|-----------------|----------------|---------|----------------------|---------|----------------------|-----------|
| BLI              | Indirect          | HEK 293T cells | UC               | Gluc            | IV             | Mice    | 30 to 360 minutes    | Biodistribution/Tumor Targeting | x         | [22]                |
|                  |                   | Melanoma cell line | UC               | Gluc            | IV             | Mice    | 10 to 240 minutes    | Biodistribution | x         | [23]                |
|                  |                   | Melanoma cell line | UC               | Gluc            | IV             | Mice    | 10 to 240 minutes    | Biodistribution | x         | [38]                |
| FLI              | Direct            | MSC             | UC               | DiD             | IV             | Mice    | 10 minutes to 24 hours | Targeting to injured kidney | x         | [12]                |
|                  |                   | Mouse B16-F10 (CRL 6475) melanoma cells | UC               | DiR             | Intradermal   | Mice    | 48 hours             | Nodal trafficking | x         | [39]                |
|                  |                   | HEK293          | UC               | DiR             | IV             | Mice    | 24 hours             | Biodistribution/Tumor Targeting | x         | [40]                |
|                  |                   | 4T1, MCF-7, and PC3 cells | Sucrose density cushion/UC | DiR             | IV and IT     | Mice    | 30 minutes to 7 hours | Biodistribution/Tumor Targeting | x         | [20]                |
| NI               | Direct            | 4T1, MCF-7, and PC3 cells | Sucrose density cushion/UC | In-oxine        | IV and IT     | Mice    | 30 min to 7 hours    | Biodistribution/Tumor Targeting | o         | [20]                |
|                  |                   | Raw 264.7, HBl.F3 | Nanovesicles (sequential filtration) iodixanol gradient/UC | $^{111}$In-oxine | IV            | Mice    | 30 minutes to 5 hours | Biodistribution | o         | [23]                |
|                  |                   | Erythrocyte     | UC               | $^{99m}$Tc-HMPAO | IV            | Mice    | 1 hour               | Biodistribution | o         | [41]                |
|                  |                   | B16BL6 murine melanoma cell line | UC               | $^{99m}$Tc-tricarbonyl | IV            | Mice    | 1 minute to 4 hours  | Biodistribution | x         | [42]                |
| MRI              | Direct            | Mouse B16-F10 (CRL 6475) melanoma cells | PureExo® Exosome Isolation Kit | USPIO           | Intradermal   | Mice    | 1 hour, 48 hours     | Nodal trafficking | o         | [43]                |
|                  |                   | Murine adipose stem cell (C57BL/6) | USPIO           | Intradermal   | Mice    | 1 hour               | Retention at injection site | o         | [19]                |

BLI, bioluminescence imaging; FLI, fluorescence Imaging; NI, nuclear imaging; MRI, magnetic resonance imaging; UC, ultracentrifuge; MSC, mesenchymal stem cell; USPIO, ultrasmall super paramagnetic iron oxide; IV, intravenous; IT, intratumor; IM, intramuscular; DiD and DiR, near-infrared dyes; Gluc, Gaussi luciferase.
assessed how targeted EVs as well as tumor burden influenced the biodistribution [75]. Nevertheless, the use of fluorescent proteins (GFP/RFP) limits the visualization of EVs in vivo. Therefore, this technique cannot be applied to visualize EVs.

A few other studies have used lipophilic dyes to label EVs in order to study their in vivo properties [12, 40, 75, 87, 88]. However, these dyes, including DiR, DiD, PKH26, and PKH67, are reported to have an in vivo half-life ranging from 5 to >100 days. Where the administered EVs have been visualized in vivo, the persistence of the dye may outlast the labeled EVs in vivo. In addition, labeling of EVs with exogenous signaling agents can result in changes to the homing characteristics of EVs, due to the labeling procedures used.

6.2. Indirect Labeling Methods. In indirect labeling, the transgene used encodes a fluorescent protein, which acts as an intrinsically produced reporter protein. Similar approaches for visualizing EVs have been proposed, and a few studies have exploited imaging based on fluorescent proteins, such as GFP, RFP, and d’Tomato, to study EVs both in vitro and in vivo [23, 72, 85, 86]. A few studies have used biomarkers in EVs, such as CD63, which was used to design a reporter conjugated to fluorescent proteins (GFP/RFP) [86, 89]. The efficiency of in vivo imaging of EVs with a fluorescent signal in mice depends on the gene expression level in the cells [90]. Unfortunately FLI of intravenously administered EVs is problematic, due to the low signal yield of the fluorescence-labeled EVs [91].

7. Tracking Extracellular Vesicles by Nuclear Imaging

Nuclear imaging is widely used for preclinical and clinical cell trafficking [77]; some nuclear imaging studies for in vivo EV monitoring (Table 1) have been published [20, 21, 41, 42]. The knowledge that has been accumulated for tracking cells with nuclear techniques can also be applied to tracking EVs. Although FLI and BLI cannot be used for effective visualization of EVs located in deep organs or tissues, due to limitation of tissue penetration of optical fluorescent and bioluminescent signals, nuclear imaging are able to visualize EVs, regardless of their location in the body, due to the excellent tissue penetration characteristics of gamma rays [91].

7.1. Direct Labeling Methods. \(^{111}\)In-oxine and \(^{99m}\)Tc-hexamethylpropyleneamineoxime (HMPAO) were widely used for labeling white blood cells in preclinical and clinical studies,
and these were also applied for tracking EVs [20, 21]. Smyth et al. labeled EVs using $^{111}$In-oxine and fluorescent dye and showed similar distribution patterns [20]. $^{111}$In-oxine could be visualized using a gamma camera or by single-photon emission computed tomography (SPECT). $^{111}$In-oxine was used for determining biodistribution only. As free $^{111}$In-oxine accumulates in the reticuloendothelial system, it is hard to distinguish whether it has been released from EVs [91]. Hwang et al. successfully labeled EVs using $^{99m}$Tc-HMPAO [21]. $^{99m}$Tc-HMPAO-labeled EVs are easily visualized using a gamma camera or SPECT. As free $^{99m}$Tc-HMPAO shows a high brain uptake and free $^{99m}$Tc is taken up by the thyroid and salivary glands, the freed form can be easily discriminated from the labeled form (Figure 4). However, a drawback of this method is the low radiochemical yield at low EV concentrations [20, 91].

Recently, $^{99m}$Tc-tricarbonyl was used for labeling EVs. $^{99m}$Tc-tricarbonyl has also been used for the labeling of a wide range of biomolecules, and it binds to several amino acids, such as histidine, methionine, and cysteine [41]. $^{99m}$Tc-tricarbonyl-labeled EVs can be visualized using a gamma camera or SPECT. This method showed relatively higher labeling efficiency in RBC-derived EVs (38.8%). However, that study only obtained 1-h images and performed image-based analysis; therefore, further investigations may be needed to track EVs over a longer time when using this method.

Radioiodine ($^{123}$I, $^{124}$I, $^{125}$I, and $^{131}$I) is commonly used for diagnosis and treatment of thyroid disease [92] and for tracking cells [93, 94]. Gamma camera and SPECT images can be obtained using $^{123}$I or $^{131}$I and positron-emission tomography (PET) images using $^{124}$I. Iodination of surface protein of the cells or transfection of sodium iodide symporter (NIS) to the cells was used for tracking the cells. Similar methods could be applied to monitor EVs in vivo. To establish more stable radioiodine-labeled EVs, a streptavidin-lactadherin fusion protein expressed in EVs was conjugated with a $^{125}$I-labeled biotin derivative [42]. Gamma camera or PET images can be obtained by changing $^{125}$I-labeled biotin to $^{123}$I-labeled biotin or $^{124}$I-labeled biotin.

7.2. Indirect Labeling Methods. Unfortunately, there are no articles about indirect radionuclide labeling EVs. Indirect radionuclide labeling methods might provide additional information. For indirect labeling, reporter gene transductions to cells before producing EVs are needed. Many kinds of nuclear reporters are already established and selection of appropriate reporter is crucial for successful in vivo EV monitoring using nuclear imaging.

8. Tracking Extracellular Vesicles by Magnetic Resonance Imaging

MRI is widely used in clinics for visualizing anatomical structures with high-resolution images. Recently, EVs were labeled with USPIOs, which shows decreased signal intensity in T2-weighted images [19, 43]. Hu et al. reported that EVs were loaded with USPIOs using electroporation (54.9 $\mu$g iron per 100 $\mu$g EV protein) [43]. After injection of the EVs into the feet of the mice, MRI successfully visualized migration of the EVs to the draining lymph nodes (Table 1).

Busato et al. labeled parent cells (adipose stem cells) with USPIOs and collected EVs from these cells [19]. As they did not manipulate the membrane of the EVs, the integrity of the EV membranes was preserved. However, the iron contents of these EVs were lower than those reported in a previous study (0.643 $\mu$g of iron per 100 $\mu$g of EV proteins) [19, 43]. They only showed decreased signal intensity after intramuscular injection of the EVs. For tracking EVs, a large amount of EVs is needed to allow visualization on MRI. Although MRI shows high-resolution images, the sensitivity of USPIOs is relatively lower than that of optical imaging or nuclear imaging [77]. Additionally, it is difficult to discriminate EVs on MR images due to the decreased signal intensity achieved with the accumulation of USPIOs.

9. Translational and Clinical Applications

Recently, EV-mediated therapies have emerged, and several clinical trials are under investigation [53, 95]. Most of the clinical trials focus on visualizing the treatment effect of EVs. Visualizing the kinetics of EVs in the human body and quantifying the EVs delivered to target lesions could reduce unnecessary effort and expenses in trials. As indirect labeling methods require gene transduction into cells before gathering EVs, which could change the biological characteristics of the cells and might cause ethical issues for clinical applications, the method might not be appropriate for clinical trials. Optical imaging technologies suffer from the intrinsic limitations
of signal penetration and therefore might not be effective in human applications. Nuclear imaging using direct labeling could be a more useful option for clinical applications, as it is safe and has no depth limitation. Radioiodine, $^{99m}$Tc, and other radionuclides are widely used in clinics; and ethical and legal problems in a clinical translation study using in vivo monitoring of EVs can be avoided by using this method. In addition, nuclear imaging technology of EVs has the benefit of theranostic potential by changing gamma ray emitting diagnostic radionuclides ($^{123}$I, $^{131}$I, $^{99m}$Tc, $^{64}$Ga, etc.) to beta-particle emitting therapeutic radionuclides ($^{131}$I, $^{90}$Y, $^{177}$Lu, etc.) [94].

10. Conclusion

In vivo imaging of EVs is important for realizing the biology and pathophysiology of EVs and for application of EVs as part of the diagnostic and therapeutic approach in various diseases. Here, we described both direct and indirect EV-labeling strategies for bioluminescent, fluorescent, nuclear, and MR imaging. Gluc combined with transmembrane domains, such as lactadherin, could reveal the spatiotemporal distribution of EVs sensitively, in a quantitative manner, in small animals without background signals. Florescent dye labeling of EVs is easy to perform, but it has the inherent disadvantage of signal generation even after EV degradation. Optical imaging has a high sensitivity without high cost but is applicable only to small animals due to the depth limitation. Nuclear imaging modalities, such as PET, SPECT, and gamma camera imaging, have problems with labeling of radionuclides but provide excellent sensitivity and easier quantification and their clinical applications are feasible. Multimodal imaging, which combines the strengths of different imaging techniques to provide corresponding information on different features of the biological process under investigation, can offer a better solution to the technical disadvantages of individual imaging modalities. An appropriate and specific labeling strategy for use with EVs should be selected for each experimental setting.

Competing Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.

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