ORTHOPAEDIC SURGERY

Risk factors for subsidence in anterior cervical fusion with stand-alone polyetheretherketone (PEEK) cages: a review of 82 cases and 182 levels

Ting-Hsien Kao · Chen-Hao Wu · Yu-Ching Chou · Hsien-Te Chen · Wen-Hsien Chen · Hsi-Kai Tsou

Abstract

Introduction  To determine risk factors for subsidence in patients treated with anterior cervical discectomy and fusion (ACDF) and stand-alone polyetheretherketone (PEEK) cages. Materials and methods  Records of patients with degenerative spondylosis or traumatic disc herniation resulting in radiculopathy or myelopathy between C2 and C7 who underwent ACDF with stand-alone PEEK cages were retrospectively reviewed. Cages were filled with autogenous cancellous bone harvested from iliac crest or hydroxyapatite. Subsidence was defined as a decrease of 3 mm or more of anterior or posterior disc height from that measured on the postoperative radiograph. Eighty-two patients (32 males, 50 females; 182 treatment levels) were included in the analysis.

Results  Most patients had 1–2 treatment levels (62.2 %), and 37.8 % had 3–4 treatment levels. Treatment levels were from C2–7. Of the 82 patients, cage subsidence occurred in 31 patients, and at 39 treatment levels. Multivariable analysis showed that subsidence was more likely to occur in patients with more than two treatment levels, and more likely to occur at treatment levels C5–7 than at levels C2–5. Subsidence was not associated with postoperative alignment change but associated with more disc height change (relatively oversized cage).

Conclusion  Subsidence is associated with a greater number of treatment levels, treatment at C5–7 and relatively oversized cage use.

Keywords  Anterior cervical discectomy · Fusion · Stand-alone · PEEK cage · Subsidence

T.-H. Kao and C.-H. Wu shared equal contribution.

T.-H. Kao · H.-K. Tsou
Functional Neurosurgery Division, Neurological Institute, Taichung Veterans General Hospital, Taichung, Taiwan, ROC
E-mail: tsouhsikai@gmail.com

T.-H. Kao
Graduate Institute of Medical Science, National Defense Medical Center, Taipei, Taiwan, ROC

T.-H. Kao
Department of Acupressure Technology, Jen-Teh Junior College of Medicine, Nursing and Management, Miaoli County, Taiwan, ROC

C.-H. Wu · W.-H. Chen
Department of Radiology, Taichung Veterans General Hospital, Taichung, Taiwan, ROC
E-mail: chenws.tw@gmail.com

Y.-C. Chou
School of Public Health, National Defense Medical Center, Taipei, Taiwan, ROC

H.-T. Chen
School of Chinese Medicine, College of Chinese Medicine, China Medical University, Taichung, Taiwan, ROC

H.-T. Chen
Department of Orthopaedic Surgery, China Medical University Hospital, Taichung, Taiwan, ROC

W.-H. Chen
Department of Medical Imaging and Radiological Sciences, College of Health Sciences, Central Taiwan University of Science and Technology, Taichung, Taiwan, ROC

H.-K. Tsou
Department of Early Childhood Care and Education, Jen-Teh Junior College of Medicine, Nursing and Management, Miaoli County, Taiwan, ROC
Introduction

Cervical spondylosis-related disorders are common problems in modern countries [1]. If supportive medical treatment and physical therapy fail to relieve clinical symptoms, and neurological deficits due to bony spurs or disc herniation are present, surgery may be indicated. Anterior cervical discectomy and fusion (ACDF) have become the standard method of treatment, and ACDF can provide adequate neural decompression and good stabilization after arthrodesis is achieved [2–4].

Many materials are used to fuse adjacent vertebral bodies including autogenous bone graft, allograft, and artificial materials [2–9]. The purposes of these materials is to maintain disc height and alignment, widen the neuroforamen, and achieve good bony fusion. Interbody cages were developed by Dr. George Bagby decades ago, were first used in a horse with Wobbler’s syndrome, and bone ingrowth through the “Bagby basket,” and fusion between two vertebral bodies occurred. Since that time many advances have occurred, and interbody cages have become a primary method for ACDF, and although there are many cage designs and materials, most of them have been shown to provide an acceptable fusion rate [5, 6, 9]. Advantages of interbody cages include less donor site morbidity, shorter operation time and early postoperative ambulation. The use of stand-alone cages is common, and most cages are designed to resist pullout through an increased friction index or shape which keeps them more stable then iliac bone graft [10]. Anterior plating and screw fixation are commonly used to increase stability, prevent graft extrusion, and increase the bone fusion rate [11]. However, implant-related complications including screw pullout, plate and screw loosening, and dysphagia are a concern [11]. While placement of a stand-alone cage for single-level disease has been shown to be effective with good outcomes, their use in contiguous multi-level disease is still unclear [12, 13].

Subsidence is a concern with the use of stand-alone cages whether for single- or multi-level disease [13–15]. Some studies have shown there is a higher rate of subsidence with titanium vs. polyetheretherketone (PEEK) cages [16, 17]. Study has also shown that the rates of subsidence are similar with or without plate and screw fixation [18]. While subsidence is a known complication with the use of interbody cages for ACDF, whether or not subsidence affects long-term outcomes is unclear, and there are few studies examining subsidence with the use of stand-alone cages [12–18].

The purpose of this study was to determine the risk factors for subsidence in patients with cervical spondylosis-related disorders treated with ACDF and stand-alone PEEK cages.

Methods

Patients

In this study, the records of patients who were diagnosed with degenerative spondylosis or traumatic disc herniation resulting in radiculopathy or myelopathy between C2 and C7 and underwent ACDF with stand-alone PEEK cages from September 2005 to June 2009 were retrospectively reviewed and approved by the ethics committee at Taichung Veterans General Hospital (CE14062). The levels of treatment depended on the clinical presentation, physical examination findings, and imaging findings. All patients received preoperative flexion–extension dynamic cervical spine plain radiographs, and magnetic resonance imaging (MRI) studies. The intervertebral cages used were made of polyetheretherketone (PEEK) (Fidji® Cervical Cage; Abbott/Zimmer, Warsaw, IN, USA). The material used to fill the cages was autogenous cancellous bone harvested from iliac crest, or hydroxyapatite, which has been shown to result in a similar fusion rate as when cancellous bone is used as the filling material [19].

Surgical procedures

All patients were operated by the same experienced spinal surgeon, and a standardized right Smith-Robinson approach was used. Affected discs were totally excised, and bony spurs resulting in nerve or spinal cord compromise were removed. The adjacent cartilage was carefully shaved and removed, and care was taken to avoid excessive bony endplate destruction. The disc space was distracted and different sized trial cages were used until an appropriate sized cage was selected according to immobility of the trial cages following distractor removal. The cage was then filled with autogenous cancellous bone harvested from the anterior iliac crest or hydroxyapatite. The implant was inserted under fluoroscopic guidance to assure exact placement. The size and depth of the implant was checked by the fluoroscopy immediately after placement at each level. After completing each level, the wound was cleaned and closed in a standard manner.

Radiographic assessment

All patients received postoperative anteroposterior (AP) and lateral plain radiographs within 1 week after surgery.
Patients were regularly followed-up, and plain radiographs of the cervical spine were obtained at 1, 3, 6, and 12 months after surgery. All radiographs were assessed by two experienced neuroradiologists blinded to the clinical status of the patients. Subsidence, fusion, and migration of the PEEK cages were evaluated on the basis of the lateral radiographs. Spinal fusion was defined as the presence of bony trabeculae across the graft-host interfaces, trabeculae bridging bone formation at the anterior and/or posterior cortex of the involved vertebral bodies, and a hazy interface between the cage and the vertebral endplate. Absence of such bridges or the presence of an anteroposterior discontinuation was classified as non-fusion. Subsidence was defined according to a method previously described [13]. Briefly, subsidence was considered to have occurred if either the anterior disc height (ADH) or posterior disc height (PDH) decreased more than 3 mm from that measured on the postoperative radiograph. The ADH, PDH, distance between the posterior margin of the titanium line of within the PEEK cage and posterior wall of the vertebral body (D-CPW), and interbody angle (IBA) were calculated as previously described [5] (Fig. 1). The interbody disc height ratio (IDHR) was defined differently with the previous article and defined as adjacent body height (x) / disc height ratio (y) (Fig. 1). If the IDHR value increased after operation, the cage size is relatively underestimated and vice versa. Difference between preoperative and postoperative disc height was defined as the ratio of preoperative IDHR/postoperative IDHR and it means relatively oversized interbody cage will cause the value increased and vice versa. In this study, the change in the ADH and PDH ratio was used as an indication of the correction of alignment after surgery.

Statistical analysis

Data were expressed as mean ± standard deviation (SD) for continuous variables, and number (percentage) for categorical variables. Characteristics between the groups with subsidence of cage and that without subsidence (yes or no) were compared by the two independent samples t test for continuous variables, and the Fisher’s exact test for categorical variables. The non-parametric Mann-Whitney test was performed to compare the number of treatment levels between male and female. A multiple generalized linear model with generalized estimating equations (GEEs) was performed with two steps to estimate odds ratios (ORs) with 95% confidence intervals (CIs) of subsidence risk for the potential risk factors. First, variables with a p value <0.1 in univariable analysis were identified, and second, these variables were included in a stepwise manner in the multivariable analysis by the forward conditional method. The Statistical Package for Social Sciences version 19.0 (SPSS, Inc., Chicago, IL, USA) was used for all statistical analyses. Values of p < 0.05 were considered to indicate statistically significance.

Results

A total of 82 patients, 32 male and 50 female, were included in the analysis. Most of the patients were diagnosed with degenerative radiculopathy or myeloradiculopathy (n = 77), and five were diagnosed as post-traumatic myeloradiculopathy without other associated injuries. Most of the patients had 1–2 treatment levels (62.2 %), and 37.8 % had 3–4 treatment levels. In total, 182 treatment levels of the 82 patients were analyzed. Treatment levels were from C2 to C7. Of the 82 patients, cage subsidence occurred in 31 patients during postoperative follow up (Table 1). Cage subsidence was not significantly associated with age (p = 0.231), but significantly associated with gender; 54.8 % of the 31 patients with subsidence were male, but only 29.4 % of the 51 patients without subsidence were male (p = 0.035). The number of discectomies was significantly associated with subsidence of the cage; 58.1 % of patients with subsidence group had 3–4 treatment levels, but only 25.5 % of patients without subsidence had 3–4 treatment levels (p = 0.005) (Table 1).

The analysis of subsidence by treatment level is presented in Table 2. Subsidence was more common when the treatment levels were C5–6 and C6–7 than when the treatment
levels were C2–3, C3–4, and C4–5 ($p = 0.003$). The more disc height change (relatively oversized cage) was significantly higher in the subsidence group than in the non-subsid-
ence group ($0.677 \pm 0.146$ vs. $0.747 \pm 0.176$, $p = 0.024$). Subsidence was not significantly associated with alignment change ($0.352$).

Thirty-nine levels (21.4%) in 31 patients (37.8%) were found as cage subsidence radiologically. The subsidence rates of all treatment levels increased during the 12 months after surgery, and were 0% at 1 week, 2.2% at 1 month, 6.6% at 3 months, 10.4% at 6 months, and to 21.4% at 12 months. There were no perioperative major complications or subsidence-related symptoms that required treatment during the 12 months follow-up postoperatively.

Results of the univariable and multivariable analysis of risk factors associated with subsidence are shown in Table 3. In univariable analyses, patients with trauma were more likely to experience subsidence than those diagnosed with cervical spondylotic radiculopathy (CSR) or cervical spondylotic myeloradiculopathy (CSMR) (OR = 1.83, $p = 0.025$), and male were more likely to experience subsidence than female (OR = 2.43, $p = 0.025$). Subsidence was more likely to occur at treatment levels C5–7 than C2–5 (OR = 3.96, $p < 0.001$). In addition, an increased disc height change was associated with a lower risk of subsidence ($0.80$, $p = 0.018$). In other words, relatively oversized cage use (decreased IDHR postoperatively) was associated with a higher risk of subsidence. Variables with $p$ value $<0.1$ in univariable analysis were stepwise included in the multivariable analysis by the forward conditional method.

Univariable analysis indicated that male had significantly more treatment levels than female (median with range: 3 [1–4] vs. 2 [1–3], $p = 0.034$), so it appeared that

Table 1 Analysis of subsidence by patient characteristics

| Data are presented as number (percentage), except for age which is presented as mean ± standard deviation |
| CSR cervical spondylotic radiculopathy, CSMR cervical spondylotic myeloradiculopathy |
| a Traffic accident or fall without endplate destruction on imaging studies |
| Total ($n = 82$) | Subsidence of cage |
| Age (year) | 57.1 ± 12.7 | 59.2 ± 13.3 | 55.7 ± 12.3 |
| Gender | | | |
| Male | 32 (39.0) | 17 (54.8) | 15 (29.4) |
| Female | 50 (61.0) | 14 (45.2) | 36 (70.6) |
| Diagnosis | | | |
| CSR and CSMR | 77 (93.9) | 27 (87.1) | 50 (98.0) |
| Traumaa | 5 (6.1) | 4 (12.9) | 1 (2.0) |

Table 2 Analysis of subsidence by treatment level

| Data are presented as number (percentage) or mean ± standard deviation |
| a Disc height change defined as the difference of the ratio of vertebra height and disc height between preoperative and postoperative radiographs |
| b Alignment change defined as the difference of the ratio of anterior disc height (ADH) and posterior disc height (PDH) between preoperative and postoperative radiographs |
| Treatment level | Total ($n = 182$) | Subsidence of cage |
| | | Yes ($n = 39$) | No ($n = 143$) |
| C2–3, C3–4, C4–5 | 100 (54.9) | 13 (33.3) | 87 (60.8) |
| C5–6, C6–7 | 82 (45.1) | 26 (66.7) | 56 (39.2) |
| Disc height changea | 0.732 ± 0.172 | 0.677 ± 0.146 | 0.747 ± 0.176 |
| Alignment changeb | 1.181 ± 0.566 | 1.282 ± 0.810 | 1.154 ± 0.479 |

Data are presented as number (percentage) or mean ± standard deviation

 Springer
gender was a confounder for the association of treatment level number and subsidence occurrence. Treatment level number, not gender, was found to be significantly associated with subsidence in the multivariable analysis; patients with more than two treatment levels were more likely to experience subsidence than those with 1–2 treatment levels (OR = 2.47, p = 0.038). In addition, subsidence was more likely to occur at treatment levels C5–7 than at levels C2–5 (OR = 3.48, p < 0.001).

Representative radiographs illustrating fusion and subsidence through the interbody space are shown in Figs. 2 and 3, respectively.

### Discussion

This study examined the risk factors of subsidence in patients with cervical spondylolytic disorders treated with ACDF and stand-alone PEEK cages. The results showed that subsidence was more likely to occur in patients with more than two treatment levels, and more likely to occur at treatment levels C5–7 than at levels C2–5. Subsidence was associated with more disc height change (relatively oversized cage) but not postoperative alignment change.

Anterior cervical discectomy was introduced by Dr. Cloward, and has become the gold standard for the treatment of cervical disc-related disease [20]. After decompression, placing an interbody bone graft can preserve disc height, widen the neuroforamen, and normalize cervical spine alignment. Rigid arthrodesis must be achieved after ACDF because of the possibility of graft dislodgement or pseudarthrosis-related complications [21]. In the past years, autogenous bone graft and allograft with plating have been used with good fusion rates [2–9]. However, donor site morbidity can occur with autogenous iliac bone graft harvesting, and allograft is not available at all hospitals. The interbody cage was developed in 1979, and a titanium cervical cage for spinal fusion surgery in humans was approved by the United States Food and Drug Administration (US FDA) in 1996. Advantages of cervical interbody cages include shorter operation time, no donor site morbidity associated with bone harvesting, and allograft is not available at all hospitals. The interbody cage was developed in 1979, and a titanium cervical cage for spinal fusion surgery in humans was approved by the United States Food and Drug Administration (US FDA) in 1996. Advantages of cervical interbody cages include shorter operation time, no donor site morbidity associated with bone harvesting, and a lower possibility of graft collapse [22, 23].

Interbody cages are designed with a high friction index to prevent pullout and increase the fusion rate, and stand-alone cervical cages are used for single- and multi-level interbody fusion by many spinal surgeons [5, 12, 13, 24–27]. Study has shown that while fusion with interbody cages may be delayed as compared to traditional bone graft, the fusion rates are similar as are the overall outcomes [6, 9, 28, 29]. Since the consistency of titanium material is not the same as the cortical bone adjacent to the cage, other materials have been developed to decrease the

### Table 3 Evaluation of risk factors of subsidence for the 182 treatment levels

| Variables                      | Univariable analysis | Multivariable analysis |
|--------------------------------|----------------------|------------------------|
|                                | OR (95 % CI)         | p value                |
|                                |                      |                        |
| Age (year)                     | 1.02 (0.99, 1.06)    | 0.247                  |
| Gender                         |                      |                        |
| Male                            | 2.43 (1.12, 5.27)    | 0.025*                 |
| Female                          | Reference group      |                        |
| Diagnosis                      |                      |                        |
| Trauma                         | 1.83 (1.08, 3.11)    | 0.025*                 |
| CSR or CSMR                    | Reference group      |                        |
| Number of treatment levels     |                      |                        |
| >2                             | 2.08 (0.96, 4.50)    | 0.062                  |
| ≤2                             | Reference group      | Reference group        |
| Treatment levels               |                      |                        |
| C5–7                           | 3.96 (1.84, 8.49)    | <0.001*                |
| C2–5                           | Reference group      | Reference group        |
| Disc height changea            | 0.80 (0.671, 0.963)  | 0.018*                 |
| Alignment changeb              | 1.45 (0.86, 2.45)    | 0.164                  |

Variables with a p value <0.1 in univariable analysis were stepwise included in the multivariable analysis by the forward conditional method.

**CSR** cervical spondylolytic radiculopathy, **CSMR** cervical spondylolytic myeloradiculopathy

* Significant impact on the occurrence of subsidence

a Disc height change defined as the difference of the ratio of vertebra height and disc height between preoperative and postoperative radiographs

b Alignment change defined as the difference of the ratio of anterior disc height (ADH) and posterior disc height (PDH) between preoperative and postoperative radiographs
Subsidence is defined as the sinking of an object with a greater elasticity modulus (e.g., cage or spacer) into an object with a lower elasticity modulus (e.g., vertebral body) [31]. In cases of ADCF with an interbody cage, this sinking can result in changes to the spinal geometry. The amount of subsidence is directly proportional to the load pressure and the difference in the elastic modulus between the two materials, and inversely proportional to the area of the interface between the two objects (i.e., cage and vertebral endplate) [31]. A large amount of subsidence can, in addition to altering spinal geometry, cause breakage or pullout of screws. Zhang et al. [32] have suggested that subsidence may be due to a process of bone incorporation between cages and vertebral endplates.
Subsidence is a concern with the use of interbody cages because it causes disc height narrowing, which can decrease the neuroforamen space created by cage distraction [13]. In the current study, the cage size was chosen by surgeon experience of the distraction force required or alignment after using trial and error method. However, there are no objective parameters to use for determining the correct size cage or for predicting the clinical outcome. Factors that have been associated with an increased risk of subsidence include poor surgical technique such as over distraction, and wrong cage size [5, 13, 27, 36]. Endplate preparation may be a factor in the occurrence of subsidence [27, 36]. Study has shown that early consolidation occurs if the endplate is removed, whereas without the removal of the endplate a fusion rate of 80% can be achieved after 6 months [37]. The bone formation processes may be different when the endplate is removed as compared to when the endplate is intact; the former may result in spongy bone growing through the cage and the latter may result in chondrogenic new bone formation [38]. It has also been reported that the incidence of subsidence is greater at the C6–7 levels [39]. Subsidence is also associated with the severity of osteoporosis [40].

There are some limitations of this study. First, while the accuracy of linear measurements on a picture archiving and communication system (PACS) is acceptable for computed tomography (CT) scans, it is inadequate for digital plain radiographs without the use of an internal calibration [41]. For this reason we used the ratio rather than the actual disc height to achieve a more precise analysis. However, cage subsidence was still defined as sinking of 3 mm or more into the endplate plane. In addition, the posterior longitudinal ligament (PLL) was excised in some cases depending on the intraoperative findings. For example, if the nerve or spinal cord was compressed by local or complete PLL ossification it was excised. On the contrary, the PLL was not completely excised if compression was due to simple nucleus pulposus herniation. Excision of the PLL was not a variable included in the analysis, and stability has been shown to be influenced by the PLL [15]. Lastly, the number of patients and the number of individual levels that received surgery were relatively small.

In conclusion, subsidence was more likely to occur in patients with more than two treatment levels, and more likely to occur at treatment levels C5–7 than at levels C2–5. Subsidence was not associated with postoperative alignment change but associated with more disc height change (relatively oversized cage). While the occurrence of subsidence does not appear to affect fusion or long-term clinical outcomes, further study is required to evaluate the significance of subsidence occurring after ACDF with PEEK cages.

Conflict of interest None.

Open Access This article is distributed under the terms of the Creative Commons Attribution License which permits any use, distribution, and reproduction in any medium, provided the original author(s) and the source are credited.

References

1. Roh JS, Teng AL, Yoo JU, Davis J, Furey C, Bohlman HH (2005) Degenerative disorders of the lumbar and cervical spine. Orthop Clin North Am 36:255–262. doi:10.1016/j.ocl.2005.01.007
2. Chen F, He W, Mahaney K, Noeler J, Mhanna N, Viljoen S, Torner J, Hitchon P (2013) Alternative grafts in
anterior cervical fusion. Clin Neurol Neurosurg 115:2049–2055. doi:10.1016/j.clineuro.2013.07.013

3. Gebremariam L, Koes BW, Peul WC, Huisstede BM (2012) Evaluation of treatment effectiveness for the herniated cervical disc: a systematic review. Spine (Phil Pa 1976) 37:E109–E118. doi:10.1097/BRS.0b013e318221b5af

4. Jacobs W, Willems PC, Kruty M, van Limbeek J, Anderson PG, Pavlov P, Bartels R, Oner C (2011) Systematic review of anterior interbody fusion techniques for single- and double-level cervical degenerative disc disease. Spine (Phil Pa 1976) 36:E950–E960. doi:10.1097/BRS.0b013e318221cbad

5. Kulkarni AG, Hee HT, Wong HK (2007) Solis cage (PEEK) for anterior cervical fusion: preliminary radiological results with emphasis on fusion and subsidence. Spine J 7:205–209. doi:10.1016/j.spine.2006.03.002

6. Lofgren H, Hee HT, Wong HK (2007) Solis cage (PEEK) for anterior cervical fusion: preliminary radiological results with emphasis on fusion and subsidence. Spine J 7:205–209. doi:10.1016/j.spine.2006.03.002

7. Marotta N, Landi A, Tarantino R, Mancarella C, Ruggeri A, Delfini R (2011) Five-year outcome of stand-alone fusion using carbon cages in cervical disc arthroplasty. Eur Spine J 20(Suppl 1):S8–S12. doi:10.1007/s00586-011-1747-0

8. Martin GJ, Jr, Haid RW, Jr, MacMillan M, Rodts GE, Jr, Berk-...
35. Wu WJ, Jiang LS, Liang Y, Dai LY (2012) Cage subsidence does not, but cervical lordosis improvement does affect the long-term results of anterior cervical fusion with stand-alone cage for degenerative cervical disc disease: a retrospective study. Eur Spine J 21:1374–1382. doi:10.1007/s00586-011-2131-9
36. van Jonbergen HP, Spruit M, Anderson PG, Pavlov PW (2005) Anterior cervical interbody fusion with a titanium box cage: early radiological assessment of fusion and subsidence. Spine J 5:645–649. doi:10.1016/j.spinee.2005.07.007 (discussion 649)
37. Porto Filho MR, Pastorello MT, Defino HL (2005) Experimental study of the participation of the vertebral endplate in the integration of bone grafts. Eur Spine J 14:965–970. doi:10.1007/s00586-004-0826-x
38. Zou X, Zou L, Foldager C, Bendtsen M, Feng W, Bunger CE (2009) Different mechanisms of spinal fusion using equine bone protein extract, rhBMP-2 and autograft during the process of anterior lumbar interbody fusion. Biomaterials 30:991–1004. doi:10.1016/j.biomaterials.2008.10.061
39. Bartels RH, Donk RD, Feuth T (2006) Subsidence of stand-alone cervical carbon fiber cages. Neurosurgery 58:502–508. doi:10.127/spine.2005.07.007 (discussion 502–508)
40. Yan D, Wang Z, Deng S, Li J, Soo C (2011) Anterior corpectomy and reconstruction with titanium mesh cage and dynamic cervical plate for cervical spondylotic myelopathy in elderly osteoporosis patients. Arch Orthop Trauma Surg 131:1369–1374. doi:10.1007/s00402-011-1317-2
41. Rampersaud YR, Fehlings MG, Harrop JS, Kuklo TR, Massicotte EM, Salonen D, Shaffrey CI, Vaccaro AR (2006) Validation of digital radiology measurement tools for quantitative spinal imaging. Top Spinal Cord Inj Rehabil 12:11–21