Dynamic contrast-enhanced perfusion parameters in ovarian cancer: Good accuracy in identifying high HIF-1α expression

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Abstract

Background
Hypoxia significantly influences treatment response and clinical outcome in solid tumors. A non-invasive marker for hypoxia will help physicians in treatment planning and encourage the efficient use of hypoxia targeted therapies. The purpose of this study was to investigate whether pharmacokinetic dynamic contrast-enhanced (DCE) perfusion parameters are associated with a specific marker of hypoxia, hypoxia-inducible factor 1 alpha (HIF-1α) in ovarian cancer (OC).

Materials and methods
Thirty-eight patients with primary OC were enrolled in this prospective study approved by the local ethical committee. Patients underwent dynamic gadolinium-enhanced 3.0 T MRI as part of their staging investigations. Pharmacokinetic perfusion parameters, including a rate constant for transfer of contrast agent from plasma to extravascular extracellular space (EES) (Ktrans) and a rate constant from EES to plasma (Kep), were measured by drawing two types of regions of interest (ROIs): a large solid lesion (L-ROI) and a solid, most enhancing small area (S-ROI) (NordicICE platform). Tissue samples for immunohistochemical analysis were collected during surgery. Kruskal–Wallis, Mann–Whitney U and Chi-square tests were used in statistical analyses. Receiver Operating Characteristic curve analyzes were done for DCE parameters to discriminate high HIF-1α expression.

Results
Pharmacokinetic perfusion parameters Ktrans and Kep were inversely associated with HIF-1α expression (Ktrans L-ROI P = 0.021; Ktrans S-ROI P = 0.018 and Kep L-ROI P = 0.032; Kep
S-ROI \( P = 0.033 \). \( K_{\text{trans}} \) and \( K_{\text{ep}} \) showed good accuracy in identifying high HIF-1\( \alpha \) expression (AUC = 0.832 \( K_{\text{trans}} \) L-ROI; 0.840 \( K_{\text{trans}} \) S-ROI; 0.808 \( K_{\text{ep}} \) L-ROI and 0.808 \( K_{\text{ep}} \) L-ROI).

**Conclusion**

This preliminary study demonstrated that pharmacokinetic DCE-MRI perfusion parameters are associated with the hypoxia specific marker, HIF-1\( \alpha \) in OC. DCE-MRI may be a useful supplementary tool in the characterization of OC tumors in a staging investigation.

**Introduction**

Ovarian cancer (OC) is one of the most lethal malignancies in women. Although the mortality rate has declined by 33% between 1976 and 2015 with reductions in both incidence and mortality, nonetheless the five-year survival rate is as low as 47% [1]. Extensive research efforts are being expended to improve the patient’s survival. Tumor hypoxia is a novel, potentially useful, target for anti-cancer drugs [2–6]. It is now well established that hypoxia is an important component of the tumor microenvironment. The growing tumor requires more oxygen and when it reaches a size of 2mm\(^3\), hypoxia occurs. Hypoxia-inducible factor 1 (HIF-1) is a heterodimer transcription factor formed from HIF-1\( \alpha \) and HIF-1\( \beta \) subunits. HIF-1\( \beta \) is a stable subunit, being constitutively expressed while HIF-1\( \alpha \) is increasingly expressed in hypoxic situations [7] and thus it has been proposed as a molecular marker of hypoxia [8]. HIF-1\( \alpha \) functions as a key regulator of the cellular response to hypoxia, modulating the expression of genes involved in processes such as metabolism, proliferation, angiogenesis and apoptosis [7,9,10]. HIF-1\( \alpha \) has shown promise as a prognostic factor in OC [11,12]. Hypoxia plays an important role in chemotherapy and radiotherapy resistance. Although OC is sensitive to chemotherapy, 70% of patients relapse [13]. This has led to studies investigating which kind of combinations of drugs or other treatment modalities would benefit patients more. HIF-1 inhibition seems to be a promising target. There are different mechanisms of action that lead to decreased HIF-1 transcriptional activity: decreased HIF-1\( \alpha \) synthesis, decreased HIF-1 DNA binding, increased HIF-1\( \alpha \) degradation and decreased HIF-1\( \alpha \) transactivation [14–18]. There are different classes of drugs effecting for these mechanisms. Several drugs have been promising in preclinical studies and are already in early clinical trials [4–6]. Current HIF-1 inhibitors suffer a nonspecific mode of action and because HIF-1 regulation comprises very complex cascade it has been very challenging task to design selective HIF-1 inhibitor, but this will be the goal in the future. It would be important to find a marker that would be predictive of hypoxia and thus help to guide treatment e.g. in devising individualized biological treatments.

Conventional magnetic resonance imaging (MRI) is applied in the preoperative imaging of indeterminate ovarian tumors due to its superior soft tissue extraction. Dynamic contrast enhanced (DCE) sequence, utilizing contrast agent extravasation from blood flow to tissues, may not only be used to characterize benign lesions from malignant tumors [19,20] but may also provide additional information on the tumor prognosis [21,22] and treatment response [23–25]. Pharmacokinetic perfusion parameters reflect the circulation physiology in the microvasculature and give quantitative parameters to compare flow and vessels permeability properties [26–28].

Few studies have correlated DCE parameters to measures of tumor oxygenation levels such as HIF-1\( \alpha \). In gliomas, there seems to be a positive correlation between HIF-1\( \alpha \) and DCE perfusion parameters [29–31], and other studies an inverse correlation has been reported [25,32].

**Competing interests**: The authors have declared that no competing interests exist.
We hypothesized that DCE-MRI could provide a noninvasive tool for the identification of tumor hypoxia also in ovarian cancer. The aim of this study was to investigate whether DCE pharmacokinetic perfusion parameters in OC would be associated with a specific marker of hypoxia, HIF-1α.

Materials and methods

Study protocol and patients

This prospective single-institution study was conducted between 2011 and 2014. The Northern Savo research ethical committee approved the study protocol (approval number 5302473) and written informed consent was obtained from all patients. A total of 38 patients was enrolled. Power calculations were not performed prospectively because no prior knowledge of the DCE parameters and HIF in OC existed, and in other cancers preliminary studies have been conducted with similar size [25,29,31,33]. The inclusion criteria included a clinical diagnosis of primary OC, primary fallopian tube cancer or primary peritoneal carcinoma, as they are diagnosed and treated as one entity and measurable disease at staging computed tomography (CT). The exclusion criteria were contraindications to MRI or to gadolinium contrast agents. All patients underwent diagnostic 3.0 T MRI before any treatment. Samples from tumors to be subjected to immunohistochemical analysis were collected during surgery. Cancers were staged using the International Federation of Gynecology and Obstetrics (FIGO) guidelines. The histological type and grade of the tumors were evaluated according to World Health Organization criteria. An experienced multidisciplinary team chose the modality of first-line treatment (surgery, n = 34; neoadjuvant chemotherapy before surgery, n = 5). Adjuvant chemotherapy after the operation was paclitaxel–carboplatin (n = 37), one patient received carboplatin monotherapy for her stage IA disease. Detailed characteristics of the patients are presented in Table 1.

Imaging protocol

MRI was performed with a 3.0 T scanner (Philips Achieva 3.0T TX, Philips N.V., Eindhoven, The Netherlands) with a body coil (Sense-XL-Torso) covering the whole abdomen from the lower thorax to the symphysis. The structured MRI protocol included transaxial, sagittal, and coronal T2-weighted sequence (repetition time (TR) 651 ms, echo time (TE) 80 ms, flip angle 90°, resolution 0.7 mm x 0.7 mm x 0.5 mm), transaxial fat-suppressed spectral attenuated inversion recovery (SPAIR) sequence (TR 744 ms, TE 70 ms, flip angle 90°), DUAL- fast field echo (FFE) sequence (TR 180 ms, TE 1.15 ms outphase and 2.30 ms inphase, flip angle 55°, resolution 1.3 mm x 1.3 mm x 5.0 mm), diffusion weighted image (DWI) sequence (TR 490 ms, TE 48 ms, flip angle 90°, resolution 1.8 mm x 1.8 mm x 5.0 mm), DCE sequences GD dyn eThrive SENSE (TR 3.8 ms, TE 1.8 ms, flip angle 10°, resolution 0.9 mm x 0.9 mm x 5.0 mm, at 6.7s intervals a total of 23 timeframes) and T1w post-contrast images (TR 6.9 ms, TE 3.5 ms, flip angle 10°, resolution 1.5 mm x 1.5 mm x 3.0 mm). During DCE image acquisition, the contrast agent gadoterate meglumine (Dotarem 279.3 mg/ml, Guerbet, France) was injected intravenously as a bolus dose of 0.1 mmol/kg at a rate of 4 ml/s using an MRI-compatible power injector (Optistart Elite, Covidien, Los Angeles, CA, USA), followed by a 20 ml flush of 0.9% sodium chloride solution.

Image analysis

Two observers (AL and OA), with 4 and 3 years of experience in gynecological imaging, evaluated all MR- and DCE- sequences blinded to the histopathological information using a Sectra PACS workstation (IDS7, Version 15.1.20.2, Sectra AB, Linköping, Sweden) and special
imaging software NordicICE (version: 2.3.13, NordicNeuroLab, Bergen, Norway). In unclear cases a senior radiologist (SR) with 12 years of experience in gynecological imaging was available for consultation. Image analysis has been described in detail previously [22]. The perfusion parameter maps were generated automatically with NordicICE using pharmacokinetic

| Variable                               | HIF-1α low | HIF-1α high | p     |
|----------------------------------------|------------|-------------|-------|
| Age *                                  | 67 [49–86] | 57 [47–72]  | 0.206 |
| BMI *                                  | 26 [17–34] | 27 [24–40]  | 0.188 |
| CA 12-5 *                              | 369 [16–1673] | 483 [69–952] | 0.957 |
| Disease variable                       | n (%)      | n (%)       |       |
| Grade                                  |            |             | 0.892 |
| 1                                      | 1 (3.3)    | 0 (0.0)     |       |
| 2                                      | 8 (26.7)   | 2 (6.7)     |       |
| 3                                      | 16 (53.3)  | 3 (10.0)    |       |
| FIGO stage                             |            |             | 0.900 |
| 1                                      | 4 (13.3)   | 1 (3.3)     |       |
| 2                                      | 2 (6.7)    | 0 (0.0)     |       |
| 3                                      | 11 (36.7)  | 2 (6.7)     |       |
| 4                                      | 8 (26.7)   | 2 (6.7)     |       |
| Histology                              |            |             | 0.952 |
| High grade serous                     | 17 (56.7)  | 3 (10.0)    |       |
| Endometrioid                           | 4 (13.3)   | 1 (3.3)     |       |
| Mucinous                               | 0 (0.0)    | 0 (0)       |       |
| Clear cell                             | 1 (3.3)    | 0 (0)       |       |
| Other histology                        | 3 (10.0)   | 1 (3.3)     |       |
| Ascites                                |            |             | 0.968 |
| No                                     | 5 (16.7)   | 1 (3.3)     |       |
| Yes                                    | 20 (66.7)  | 4 (13.3)    |       |
| Residual tumor at primary surgery      |            |             | 0.348 |
| No                                     | 14 (46.7)  | 1 (3.3)     |       |
| ≤1 cm                                  | 9 (30.0)   | 3 (10.0)    |       |
| >1 cm                                  | 2 (6.7)    | 1 (3.3)     |       |
| Tumor recurrence                       |            |             | 0.692 |
| No                                     | 10 (40.0)  | 1 (4.0)     |       |
| Yes                                    | 12 (48.0)  | 2 (8.0)     |       |
| Platinum sensitivity                   |            |             | 0.428 |
| Sensitive                              | 20 (66.6)  | 3 (10.0)    |       |
| Resistance                             | 5 (16.7)   | 2 (6.7)     |       |
| Chemotherapy response                  |            |             | 0.395 |
| Complete response                      | 20 (66.6)  | 3 (10.0)    |       |
| Partial response                       | 2 (6.7)    | 0 (0)       |       |
| Stable disease                         | 0 (0)      | 0 (0)       |       |
| Progressive disease                    | 3 (10.0)   | 2 (6.7)     |       |

HIF-1α expression has been dichotomized into low and high using the median immunoreactive score as the cutoff value

*Results are median with range in square brackets

BMI = body mass index, FIGO = the International Federation of Gynecology and Obstetrics

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modeling of contrast kinetics according to the Tofts model [28]. Motion correction was done automatically at first. The perfusion was quantified by determining the arterial input function (AIF) by drawing a small AIF ROI onto the common or external iliac arteries. According to clinical practice at the time of study designing, B1 maps and T1 mapping were not used. Four quantitative parameters were measured as follows; 1. $K_{\text{trans}}$, a rate constant for the transfer of contrast agent from plasma to the extravascular extracellular space (EES), 2. $K_{\text{ep}}$, a rate constant from EES to plasma; 3. $V_e$, contrast agent distribution volume and 4. $V_p$, fractional plasma volume. All measurements were obtained using the transaxial images showing the largest solid tumor diameters in the ovary. Two regions of interests (ROIs) were used; first a large ROI (L-ROI) was drawn free-hand to cover the whole solid tumor area, excluding cystic, necrotic and vascular areas. A small circle ROI (S-ROI), with a set size of 15×15 pixels, was then placed on the area considered to be the most solid and intensively enhancing. T2w-, T1w-, DWI-, and contrast-enhanced T1w- images were all available for tumor localization and ROI delineation. The ROIs were then replicated to the DCE parameter maps illustrated in Fig 1. Mean values were registered for each DCE parameter in the analyses.

Immunohistochemistry

The tissue samples from tumors were embedded in paraffin and cut into 5-µm-thick sections. The sections were processed for hematoxylin-eosin and HIF-1α (Novus 1:75, United...
Kingdom) staining. An experienced pathologist selected the most representative samples, i.e. those with the most tumoral component in routine hematoxylin and eosin-stained slides, which were then examined with immunohistochemical staining (HIF-1α). The HIF-1α expression was analyzed from the nuclei of the epithelial OC cells (Fig 2) and was scored semiquantitatively using the immunoreactive score (IRS)[34,35]. In brief, IRS is the multiplication of staining intensity (0 = negative, 1 = weak, 2 = moderate and 3 = strong) and the description for percentage of positive cells (0 = negative, 1 = 1–10%, 2 = 11–50%, 3 = 51–75% and 4 = 76–100%). The median IRS value was used as a cutoff for low and high expression.

Statistical analysis

SPSS for Windows (Version 22.0, 2013, SPSS Inc., Chicago, IL, USA) was used for statistical analysis. Values are presented as mean ± SD unless otherwise stated. The Intraclass correlation coefficient (ICC) was used in interobserver reproducibility analysis. For classified parameters, Kruskal–Wallis and Mann–Whitney U tests were used when appropriate. Chi-square test was used for frequency tables. P ≤ 0.05 was considered statistically significant. Analysis of receiver operating characteristic (ROC) curves was performed for DCE pharmacokinetic perfusion parameters to discriminate between low and high levels of HIF-1α expression. The area under the curve (AUC) was classified as “low” (0.5–0.7), “moderate to good” (0.7–0.9) and “very good to excellent” (0.9–1). The values of AUC, specificity, sensitivity, positive predictive value (PPV), negative predictive value (NPV) and cutoff value were calculated. The most appropriate cutoff values were determined according to the highest Youden Index (sensitivity + specificity -1) from estimate curves. Association of these cutoff values with HIF-1α expression was tested with Chi-square test.

Results

A total of 38 patients were recruited. Three patients were excluded from DCE imaging analyses due to insufficient image quality: two due to movement artifacts and one because of a different scanning time. The five patients who received neoadjuvant chemotherapy were excluded from the histopathological analysis. Thus, altogether 30 patients with primary OC (mean age 66 years, range 47–86 years) were included (Table 1). Staging operation was performed within 7 ± 6 days after imaging. The largest diameter for the solid tumor component was 77 mm (range 23–233 mm). Intraclass correlation coefficient (ICC) were excellent for DCE perfusion parameters $K_{\text{trans}}$, $K_e$ and $V_e$ ($K_{\text{trans}}$ L-ROI 0.994 and S-ROI 0.980; $K_e$ L-ROI 0.985 and S-ROI 0.921; $V_e$ L-ROI 0.997 and S-ROI 0.964) but for $V_p$ only good to moderate (L-ROI 0.621 and S-ROI 0.598).

HIF-1α expression in ovarian cancer

In this cohort, HIF-1α expression was low in 26 (84%) and high in 5 (16%) patients (Fig 2). HIF-1α was low in 80% (4/5) of stage I, 100% (2/2) of stage II, 85.7% (12/14) of stage III and 80% (8/10) of stage IV tumors and correspondingly, in stages I–IV, high in 20% (1/5), 0% (0/2), 14.3% (2/14) and 10% (2/10). HIF-1α did not associate significantly with the FIGO stage ($P = 0.900$). In addition, HIF-1α expression was independent of patient’s age ($P = 0.206$) and CA-125 levels ($P = 0.957$) as well as of histological grade ($P = 0.892$) and subtype of the tumor ($P = 0.952$). Furthermore, the expression of HIF-1α did not associate with the result of surgical operation, response to treatment, platinum sensitivity or to tumor recurrence (Table 1).

HIF-1α association with DCE parameters

HIF-1α expression was inversely associated with $K_{\text{trans}}$ and $K_e$ values (Fig 3). Association was significant for both L- and S-ROIs ($K_{\text{trans}}$ L-ROI $P = 0.021$ and S-ROI $P = 0.018$; $K_e$ L-ROI...
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$P = 0.032$ and S-ROI $P = 0.033$). HIF-1$\alpha$ expression did not associate with $V_e$ or $V_p$ values (Table 2). Analysis of the ROC curve demonstrated good accuracy for DCE parameters $K_{\text{trans}}$ and $K_{\text{ep}}$ in discriminating between low and high HIF-1$\alpha$ expression, with AUCs of 0.832 for $K_{\text{trans}}$ L-ROI, 0.840 for $K_{\text{trans}}$ S-ROI, 0.808 for $K_{\text{ep}}$ L-ROI and 0.808 for $K_{\text{ep}}$ S-ROI (Fig 4). A summary of AUC, cutoff values, sensitivity, specificity, PPV, NPV and Youden Index for $K_{\text{trans}}$ and $K_{\text{ep}}$ are presented in Table 3.
The following cutoff values were further used to dichotomize the \( K_{\text{trans}} \) and \( K_{\text{ep}} \) values into low or high: 0.375 (L-ROI), 0.487 (S-ROI) for \( K_{\text{trans}} \) and 0.874 (L-ROI) and 1.071 (S-ROI) for \( K_{\text{ep}} \). These dichotomized DCE parameters proved to be statistically significantly associated with HIF-1\( \alpha \) expression (\( K_{\text{trans}} \) L-ROI \( P = 0.003; \) \( K_{\text{trans}} \) S-ROI \( P = 0.003; \) \( K_{\text{ep}} \) L-ROI \( P = 0.047 \) and \( K_{\text{ep}} \) S-ROI \( P = 0.017 \)).

### Discussion

This study investigated the association between the hypoxia specific marker, HIF-1\( \alpha \), and pharmacokinetic perfusion parameters measured by DCE MR imaging in OC. There was a significant inverse association between HIF-1\( \alpha \) and \( K_{\text{trans}} \) and \( K_{\text{ep}} \) values. Based on the ROC analysis, \( K_{\text{trans}} \) and \( K_{\text{ep}} \) values proved to be good discriminators for identifying low and high HIF-1\( \alpha \) expression (\( K_{\text{trans}} \) L-ROI \( P = 0.003; \) \( K_{\text{trans}} \) S-ROI \( P = 0.003; \) \( K_{\text{ep}} \) L-ROI \( P = 0.047 \) and \( K_{\text{ep}} \) S-ROI \( P = 0.017 \)).

\( K_{\text{trans}} \) is a rate constant reflecting the contrast agent’s flow from plasma to the extravascular, extracellular space (EES); \( K_{\text{ep}} \) is the rate constant for transfer of contrast agent from EES to plasma, \( V_e \) = contrast agent distribution volume, \( V_p \) = plasma volume fraction.

Results are mean ± standard deviation (SD). HIF-1\( \alpha \) has been dichotomized using the median immunoreactive score as the cutoff value.

\( K_{\text{trans}} \) and \( K_{\text{ep}} \) for distinguishing low and high HIF-1\( \alpha \) is shown in Table 3. The following cutoff values were further used to dichotomize the \( K_{\text{trans}} \) and \( K_{\text{ep}} \) values into low or high: 0.375 (L-ROI), 0.487 (S-ROI) for \( K_{\text{trans}} \) and 0.874 (L-ROI) and 1.071 (S-ROI) for \( K_{\text{ep}} \). These dichotomized DCE parameters proved to be statistically significantly associated with HIF-1\( \alpha \) expression (\( K_{\text{trans}} \) L-ROI \( P = 0.003; \) \( K_{\text{trans}} \) S-ROI \( P = 0.003; \) \( K_{\text{ep}} \) L-ROI \( P = 0.047 \) and \( K_{\text{ep}} \) S-ROI \( P = 0.017 \)).

### Table 2. The associations between the expression of hypoxia-inducible factor 1alpha (HIF-1\( \alpha \)) and various perfusion parameters.

|         | HIF-1\( \alpha \) low | HIF-1\( \alpha \) high | \( p \)-value |
|---------|------------------------|------------------------|--------------|
| \( K_{\text{trans}} \) L-ROI | 0.88 (0.96)            | 0.30 (0.07)            | 0.021        |
| \( K_{\text{trans}} \) S-ROI | 0.95 (1.12)            | 0.39 (0.14)            | 0.018        |
| \( K_{\text{ep}} \) L-ROI | 1.19 (0.58)            | 0.62 (0.46)            | 0.032        |
| \( K_{\text{ep}} \) S-ROI | 1.21 (0.54)            | 0.68 (0.43)            | 0.033        |
| \( V_e \) L-ROI | 85.07 (91.60)          | 50.74 (35.79)          | 0.388        |
| \( V_e \) S-ROI | 93.33 (102.46)         | 66.59 (48.22)          | 0.420        |
| \( V_p \) L-ROI | 9.43 (7.99)            | 15.30 (14.20)          | 0.419        |
| \( V_p \) S-ROI | 10.67 (8.87)           | 18.98 (15.50)          | 0.488        |

Results are mean ± standard deviation (SD). HIF-1\( \alpha \) has been dichotomized using the median immunoreactive score as the cutoff value.

\( K_{\text{trans}} \) = the rate constant for transfer of contrast agent from plasma to extravascular, extracellular space (EES); \( K_{\text{ep}} \) = the rate constant for transfer of contrast agent from EES to plasma, \( V_e \) = contrast agent distribution volume, \( V_p \) = plasma volume fraction.

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Tumors with low oxygenation levels start to induce the expression of HIF-1\( \alpha \) which is an important factor for tumor growth e.g. allowing the tumor cells to adapt to a hypoxic environment and regulating the production of pro-angiogenic factors [9]. Interestingly, in this study, \( K_{\text{trans}} \) and \( K_{\text{ep}} \) were inversely associated with HIF-1\( \alpha \) expression. The published results between tumor oxygenation and DCE perfusion parameters in different types of malignancies are somewhat conflicting (Table 4). As far as we are aware, no prior studies have investigated this correlation in OC.

In gliomas, Xie et al. showed that HIF-1\( \alpha \) was correlated positively with \( K_{\text{trans}} \) and \( V_e \) values [29]. These investigators used stereotactic biopsies for histopathological samples, to minimize the mismatch of measurements. In another study with gliomas, a positive correlation was
observed between HIF-1α and relative cerebral blood volume, but in that study, the expression level of HIF-1α did not correlate significantly with either $K_{\text{trans}}$ or $K_{\text{ep}}$ values [30]. Jensen et al. examined glioblastoma specimens and noted that HIF-1α correlated positively with blood volume and capillary transit time [31]. In their study, higher perfusion parameters were

![Image of ROC curves](https://doi.org/10.1371/journal.pone.0221340.g004)

Fig 4. Analysis of ROC curves for the two DCE perfusion parameters, $K_{\text{trans}}$ and $K_{\text{ep}}$, in the discrimination between low and high HIF-1α expression. The analysis reveals the diagnostic accuracy of A) $K_{\text{trans}}$ L-ROI (AUC = 0.832) B) $K_{\text{trans}}$ S-ROI (AUC = 0.840), C) $K_{\text{ep}}$ L-ROI (AUC = 0.808) and D) $K_{\text{ep}}$ S-ROI (AUC = 0.808). HIF-1α expression dichotomized into low and high using the median immunoreactive score as the cutoff value.
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Table 3. Analyses of receiver operating characteristic (ROC) curves of DCE perfusion parameters to discriminate between low and high expression of hypoxia-inducible factor 1 alpha (HIF-1α).

| Study            | Tumor type      | N   | MRI  | DCE variables | Histopathological variables | HIF-1α correlation |
|------------------|-----------------|-----|------|---------------|-----------------------------|-------------------|
| Borren[33]       | prostate cancer | 15  | 3 T  | Ktrans, Kep   | HIF-1α and HIF-2α            | No correlation    |
| Loncaster[25]    | cervical cancer | 35  | 1.5 T| Amplitude, Kep | Po, graph                    | Po, inverse correlation |
| Halle[32]        | cervical cancer | 78  | 1.5 T| brix model, A430, Kep, Kd   | HIF-1α            | Inverse correlation |
| Berg[41]         | endometrial cancer | 164 | 1.5 T| blood flow, Ktrans, Kep, Ve, Fb, IAUGC, ADC | HIF-1α            | No correlation |
| Xie[29]          | glioma          | 34  | 3 T  | Ktrans, Kep, Ve, Vp | HIF-1α                   | Positive correlation |
| Awasthi[30]      | glioma          | 76  | 1.5 T| rCBV, rCBF, Ktrans, Kep, Ve | HIF-1α, vgf, prl-3, MMP-9 | Positive with rCBV, and VEGF expression |
| Jensen[31]       | glioblastoma    | 16  | 1.5 T, 3 T | F, E, PS, Ktrans, Kep, Ve, Vp, tc, α−1 | HIF-1α, VEGF, CA-IX, GLUT-1 | Positive with tc and Vb |
| Present study    | ovarian cancer  | 30  | 3 T  | Ktrans, Kep, Ve, Vp | HIF-1α                   | Inverse association |

N = number of patients, MRI = magnetic resonance imaging, T = tesla, Ktrans = a rate constant for transfer of contrast agent from plasma to extravascular, extracellular space (EES); Kep = a rate constant for transfer of contrast agent from EES to plasma, A430 = amplitude, Kd = the transfer rate of tracer from tissue to plasma, Ke4 = the clearance rate of the tracer from plasma, Ve = contrast agent distribution volume, EES volume fraction, Fb = blood flow, IAUGC = integrated area under the concentration time curve, Ve = plasma volume fraction, rCBV = relative cerebral blood volume, rCBF = relative cerebral blood flow, CER = contrast enhancement ratio, PR = pattern recognition technique, F = tumor blood flow, E = extraction fraction, PS = permeability surface area product, Vb = blood volume, tc = capillary transit time, and α−1 = capillary heterogeneity, HIF-1α = Hypoxia-inducible factor 1alpha, VEGF = vascular endothelial growth factor, CA-IX = carbonic anhydrase IX, and GLUT-1 = glucose transporter-1

AUC = area under the curve; CI = confidence interval; PPV = positive predictive value, NPV = negative predictive value; Youden Index = sensitivity + specificity - 1

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Table 4. Studies that have examined the relationships between oxygenation and DCE perfusion parameters.

| Tumor type | N | MRI | DCE variables       | Histopathological variables | HIF-1α correlation |
|------------|---|-----|---------------------|-----------------------------|-------------------|
| Present study | 30 | 3 T | Ktrans, Kep, Ve, Vp | HIF-1α                    | Inverse association with Ktrans and Kep |

associated with worse outcome [31]. One explanation for the difference in the correlation direction between gliomas and OC might be the blood brain barrier. It is possible that the distribution of the contrast agent is different in OC as compared to brain tumors, in the latter case, the contrast has first to penetrate through the blood brain barrier.

On the other hand, studies in cervical cancer have shown that higher levels of tumor perfusion and permeability are associated with a better prognosis [38,39]. It has been postulated that highly enhancing tumors are better oxygenated [38,39]. Should that be the case, also the levels of HIF-1α should be lower when perfusion parameters are high as HIF-1α starts to increase in a hypoxic environment. This proposal would help to interpret the results of this study where an inverse association was detected between HIF-1α and DCE perfusion parameters.

In part paralleling the results of the present study, Loncaster et al. examined a cohort of 35 patients with cervical cancer and reported that oxygenation status correlated inversely with...
K<sub>ep</sub> levels [25]. The authors used the Eppendorf Po<sub>2</sub> histograph method for evaluating the oxygenation level and the possible correlation between oxygenation and K<sup>trans</sup> levels was not studied. Another study in cervical cancer showed that HIF-1α upregulation was associated with low Amplitude in the Brix model (A<sub>Brix</sub>) [32]. Even when using a different model for interpreting the pharmacokinetic data, they also obtained an inverse association between HIF-1α and A<sub>Brix</sub>, a parameter reflecting interstitial and blood volume [32,40].

In a study of prostate cancer patients, neither HIF-1α nor -2α correlated with K<sup>trans</sup> or K<sub>ep</sub> values [33], but there were only 15 patients in the final analysis. When patients with endometrial cancer were examined, the expression levels of HIF-1α did not show any correlation with K<sup>trans</sup> or K<sub>ep</sub> values, however a low tumor blood flow was associated with a hypoxia gene signature and HIF-1α expression [41].

It has been shown that cancer can elevate HIF-1α levels in both an oxygen-dependent and independent manner. HIF-1α expression increases through the oxygen-dependent pathway in hypoxic situations; it facilitates adaptation to oxygen deprivation, for example by regulating the expression of several genes which control glucose uptake, metabolism, angiogenesis, erythropoiesis, cell proliferation, and apoptosis [9,10]. In the hypoxia-independent pathway, increased oncogenic signaling in cancer cells induces HIF-1α expression [42–44]. These two pathways may partly explain the discrepancy in the literature regarding the association between HIF-1α expression and K<sup>trans</sup> or K<sub>ep</sub> in different tumors. Hypothetically, HIF-1α expression may be more dependent on the oxygen-dependent pathway in fast-growing, highly proliferative, tumors such as OC than in slow-growing tumors.

In glioma studies, the expression of HIF-1α has been correlated positively with tumor grade [29,30], which is a strong prognostic factor for survival in gliomas. In the present study of patients with OC, we observed no correlation of HIF-1α expression with either clinical prognostic factors or grade. This is in accordance with some other studies in OC [11,45]. Furthermore, in the present study, we did not detect any correlation between primary treatment results and HIF-1α expression, although this may be related to the small size of our cohort.

The results of the present study suggest that K<sup>trans</sup> and K<sub>ep</sub> are good indicators for differentiating tumors with low vs. high HIF-1α expression levels in OC. In the ROC curve analysis, K<sup>trans</sup> and K<sub>ep</sub> displayed good accuracy to detect high HIF-1α expression. PPV was slightly better for K<sup>trans</sup> than for K<sub>ep</sub> values. When we further dichotomized the DCE parameters into low or high they proved to be significantly associated with the HIF-1α expression. No earlier studies have calculate cutoff points for DCE parameters to determine high HIF-1α expression in OC.

There are some limitations to these findings. Firstly, the sample size was only 30 patients. Secondly, there is a possibility of some mismatch between the site of histopathological samples and ROI placements. In OC, the tumors are located deep in the pelvis, preventing any kind of stereotactic biopsy for sampling the cancer. Histopathological samples were obtained from radically resected tumors, from which the pathologist chose the most representative part of the tumor for immunohistochemical analyses. S-ROI has been delineated in the same area of tumor as the pathological sample, but still the possibility of mismatch remains. In our study protocol, the acquisition time was 6.7sec/stack in the perfusion scan for 51 slices with an acquisition matrix of 267<sup>3</sup> 387. T1 maps were not included because the imaging protocol was already time-consuming. The AIF shape was inspected individually as being accurate for all patients. B1 correction was not performed. In future studies, a shorter temporal resolution could yield data that are more robust. In addition, when comparing results from different investigators and institutions, only results from studies that have used similar MR scanners, scanning protocols and DCE analysis are directly comparable.
In conclusion, the results of the present study suggest that in patients with OC, the expression level of hypoxia-inducible factor 1 alpha (HIF-1α) is inversely associated with tumor pharmacokinetic DCE-MRI perfusion parameters $K_{\text{trans}}$ and $K_{\text{ep}}$. If it were possible to detect the poorly oxygenated tumors preoperatively, this could help the physician to make decisions of treatment modalities and encourage the efficient use of hypoxia-modifying therapies [43,46]. Although DCE MRI may become a valuable imaging tool for detailed OC tumor characteristic screening, more trials will need to be completed before it becomes part of the clinical routine.

Supporting information

S1 Table. Characteristics and measurements of the study population.
(XLSX)

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