Solution of fractional bioheat equation in terms of Fox’s H-function

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Abstract

Present paper deals with the solution of time and space fractional Pennes bioheat equation. We consider time fractional derivative and space fractional derivative in the form of Caputo fractional derivative of order $\alpha \in (0, 1]$ and Riesz–Feller fractional derivative of order $\beta \in (1, 2]$ respectively. We obtain solution in terms of Fox’s H-function with some special cases, by using Fourier–Laplace transforms.

Keywords: Fractional bioheat equation, Caputo derivative, Riesz–Feller derivative, Fox’s H-function

Mathematics Subject Classification: 26A33, 35R11, 80A20

Background

The transfer of heat in skin tissue is mainly a heat conduction process, which is coupled to several additional complicated physiological process, including blood circulation, sweating, metabolic heat generation and sometimes heat dissipation via hair or fur above the skin surface (Ozisik 1985). Accurate description of the thermal interaction between vasculature and tissue is essential for the advancement of medical technology in treating fatal disease such as tumors and skin cancer. Mathematical model has been used significantly in the analysis of hyperthermia in treating tumors, cryosurgery, fatal-placental studies, and many other applications (Minkowycz et al. 2009).

Fractals and fractional calculus have been used to improve the modelling accuracy of many phenomena in natural science. The most important advantage of using fractional calculus approach is due to its non-local property. This means that the next state of a system depends not only upon its current state but also upon all of its historical states. Many researchers worked on fractional partial differential equations and gave very important results. Mainardi et al. (2005) obtained the fundamental solution of Cauchy problem for the space–time fractional diffusion equation in terms of H-function, Langlands (2006) gave the solution of a modified fractional diffusion equation on an infinite domain, Salim and El-Kahlout (2009) discussed exact solution of time fractional advection dispersion equation with reaction term, Saxena et al. (2006) obtained solution of generalized fractional kinetic equation in terms of Mittag-Leffler function, Haubold et al. (2011) obtained solution of a fractional reaction diffusion equation in closed form, Huang and Guo (2010) gave the fundamental solutions to a class of the time fractional
partial differential equation for Cauchy problem in a whole-space domain and signalling problem in a half-space domain. Shang (2015) gave analytic solution of viral infection dynamics in vivo through a time-inhomogeneous Markov chain characterization by Lie algebraic approach.

In present study, we consider fractional form of Pennes bioheat equation by replacing first order time derivative by Caputo fractional derivative of order $\alpha \in (0,1]$ and second order space derivative by Riesz–Feller fractional derivative of order $\beta \in (1,2]$ respectively. We make an attempt to solve the fractional model by dividing it into two sections. In section one, time fractional derivative is considered while in section two, space fractional derivative is taken into account. We apply Laplace–Fourier transform and obtain the solution in term of Fox H-function.

**Preliminaries and notations**

Fractional derivative of order $\alpha$ is denoted as $aD_1^\alpha f(t)$, the subscripts $a$ and $t$ denote the two limits related to the operation of fractional differentiation, which are called the terminal of fractional differentiation. If $\alpha$ is negative then it denotes the fractional integrals of arbitrary order.

**Definition 1** (Kilbas et al. 2006) The Riemann–Liouville fractional derivative of order $\alpha > 0$ for $\text{Real}(\alpha) > 0$ and $m \in N, t > a$ is defined as

\[
aD_1^\alpha f(t) = \left\{ \begin{array}{ll}
\frac{d^m}{dt^m} \left[ \frac{1}{\Gamma(m-\alpha)} \int_a^t f(\tau) \frac{1}{(t-\tau)^{\alpha+1-m}} d\tau \right], & \text{for } m - 1 < \alpha < m \\
\frac{d}{dt} f(t), & \text{for } \alpha = m.
\end{array} \right.
\]

(1)

**Definition 2** (Kilbas et al. 2006) The Caputo fractional derivative of order $\alpha > 0$, for $\text{Real}(\alpha) > 0$ and $m \in N, t > a$ is defined as

\[
cD_1^\alpha f(t) = \left\{ \begin{array}{ll}
\frac{1}{\Gamma(m-\alpha)} \int_a^t f^{(m)}(\tau) \frac{1}{(t-\tau)^{\alpha+1-m}} d\tau, & \text{for } m - 1 < \alpha < m \\
\frac{d}{dt} f(t), & \text{for } \alpha = m.
\end{array} \right.
\]

(2)

**Definition 3** (Kilbas et al. 2010) The Laplace transform of function $f(t)$ denoted by $F(s), s$ being the complex variable is defined as

\[
F(s) = \mathcal{L}\{f(t)\} = \int_0^\infty e^{-st} f(t) dt; \quad t \in R^+
\]

(3)

Inverse Laplace transform of $F(s)$ is defined as

\[
f(t) = \mathcal{L}^{-1}\{F(s)\} = \frac{1}{2\pi i} \int_{y-i\infty}^{y+i\infty} e^{st} F(s) ds; \quad t \in R^+, y = R(s).
\]

(4)

Laplace transform of Caputo derivative (Podlubny 1999) is given as

\[
\mathcal{L}\{c_0D_1^\alpha f(t)\} = s^\alpha F(s) - \sum_{k=0}^{n-1} s^{\alpha-k-1} f^k(0), \quad n - 1 < \alpha \leq n.
\]

(5)
**Definition 4** (Debnath and Bhatta 2007) The Fourier transform of a function \( f(x) \) is denoted by \( F^*(k) \) and defined as

\[
F(f(x)) = F^*(k) = \int_{-\infty}^{\infty} e^{-ikx} f(x) \, dx,
\]

where, \( f(x) \) is continuous and absolutely integrable in \(( -\infty, \infty)\). Inverse Fourier transform is defined as

\[
F^{-1}(F^*(k)) = \frac{1}{2\pi} \int_{-\infty}^{\infty} e^{ikx} F^*(k) \, dk.
\]

Fourier cosine transform and Inverse Fourier cosine transform are defined as (Debnath and Bhatta 2007)

\[
F_c(f(x)) = F_c^*(k) = \int_{0}^{\infty} \cos(kx) f(x) \, dx,
\]

\[
F_c^{-1}(F_c^*(k)) = f(x) = \frac{2}{\pi} \int_{0}^{\infty} \cos(kx) F_c(k) \, dk.
\]

The Fourier convolution of two functions is defined (Debnath and Bhatta 2007) as

\[
h \ast \phi = (h \ast \phi)(x) = \frac{1}{2\pi} \int_{-\infty}^{\infty} h(x-t) \phi(t) \, dt.
\]

**Definition 5** (Kilbas et al. 2010) The Mellin transform of a function \( \phi(t) \) is defined as

\[
(M\phi)(p) = M[\phi(t)](p) = \phi^*(s) = \int_{0}^{\infty} t^{s-1} \phi(t) \, dt; \quad t \in R^+(0, \infty), \ s \in C.
\]

and inverse Mellin transform as

\[
(M^{-1}g)(x) = M^{-1}[g(s)](x) = \frac{1}{2\pi i} \int_{\gamma-i\infty}^{\gamma+i\infty} x^{-s} g(s) \, ds; \quad x \in R^+, \ \gamma = R(s).
\]

**Definition 6** (Kilbas et al. 2006) Riesz–Feller partial fractional derivative \( \left(D_{\theta,x}^\beta u\right)(x,t) \) defined, for \( 0 < \beta < 2 \) and \( |\theta| \leq \min \{ \beta, 2 - \beta \} \) via the Fourier transform, by

\[
\left(F_x D_{\theta,x}^\beta u\right)(\sigma,t) = |\sigma|^\beta e^{i\left(\text{sign}(\sigma)\frac{\sigma t}{2}\right)} \left(F_x u\right)(\sigma,t); \quad \sigma \in R; \ t > 0.
\]

**Definition 7** (Podlubny 1999) Mittag-Leffler function for one parameter is denoted by \( E_{\alpha}(z) \) and defined as

\[
E_{\alpha}(z) = \sum_{k=0}^{\infty} \frac{z^k}{\Gamma(\alpha k + 1)}, \quad \alpha > 0.
\]
Mittag-Leffler function for two parameter is denoted by $E_{\alpha,\beta}(z)$ and defined as

$$E_{\alpha,\beta}(z) = \sum_{k=0}^{\infty} \frac{z^k}{\Gamma(\alpha k + \beta)}, \quad \alpha > 0, \beta > 0.$$  \hspace{1cm} (15)

Podlubny (1999) reported the Laplace transform of a derivative of Mittag Leffler function as

$$L(t^{\alpha n+\beta-1}E_{\alpha,\beta}^n(\pm at^\alpha)) = \frac{s^{\alpha-\beta} \Gamma(n+1)}{(s^\alpha + a)^{n+1}},$$  \hspace{1cm} (16)

and inverse Laplace transform of (16) is also existing as

$$L^{-1}\left(\frac{s^{\alpha-\gamma}}{(s^\alpha + a)^{n+1}}\right) = \frac{1}{\Gamma(n+1)} t^{\alpha n+\gamma-1}E_{\alpha,\gamma}^n(\pm at^\alpha).$$  \hspace{1cm} (17)

**Definition 8** (Mathai et al. 2010) The H-function is defined by means of a Mellin–Barners type integral in the following manner

$$H(z) = H_{p,q}^{m,n} \left( \frac{(a_p A_p)}{(b_q B_q)} \right) = H_{p,q}^{m,n} \left( z^{(a_1, A_1), \ldots, (a_p, A_p)} \right)$$

$$= \frac{1}{2\pi i} \int_{L} \Theta(s) z^{-s} ds,$$

where,

$$i = \sqrt{-1}, \quad z \neq 0, \quad z^{-s} = \exp(-s \log |z| + i \arg z),$$

$$\Theta(s) = \frac{\prod_{j=1}^{m} \Gamma(b_j + B_j s) \prod_{j=m+1}^{n} \Gamma(1 - a_j - A_j s)}{\prod_{j=m+1}^{n} \Gamma(1 - b_j - B_j s) \prod_{j=1}^{p} \Gamma(a_j + A_j s)}.$$  \hspace{1cm} (18)

and an empty product is interpreted as unity, $m, n, p, q \in N_0$ with $0 \leq n \leq p, 0 \leq m \leq q$, $A_j, B_j \in R_+, a_j, b_j \in C$, $j = 1, \ldots, p$; $j = 1, \ldots, q$, such that $A_j(b_j + k) \neq B_j(a_j - \lambda - 1)$, $k, \lambda \in N_0; \quad j = 1, \ldots, n; \quad j = 1, \ldots, m$. where $N_0 = 0, 1, 2, \ldots, R = (-\infty, \infty), \quad R_+ = (0, \infty)$ and $C$ being the complex number field. The counter $\Omega$ is infinite contour which separates all the poles of $\Gamma(1 - a_j + sA_j)$, $j = 1, \ldots, n$.

The relation between derivative of Mittag-Leffler function and H-Function (Langlands 2006) is given as

$$E_{\alpha,\beta}^m(\eta) = H_{1,2}^{1,1} \left[ -\eta^{(m-1)}(0,1),(1-\alpha m-\beta, \alpha) \right].$$  \hspace{1cm} (19)

**Fractional bioheat equation**

The Pennes bioheat model (Pennes 1948) is widely used for study of the heat transfer in skin tissue due to its simplicity, ease application and effectiveness. Pennes (1948) suggested that the rate of heat transfer between blood and tissue is proportional to the product of the volumetric perfusion rate and difference between the arterial blood temperature and the local tissue temperature. Pennes equation is employed to describe the heat transfer process as
\[ \rho c \frac{\partial T}{\partial t} = k \frac{\partial^2 T}{\partial x^2} + W_b c_b (T_a - T) + Q_{\text{met}} + Q_{\text{ext}}, \]  

(20)

where \( \rho, c \) and \( k \) represent density, specific heat and thermal conductivity respectively. \( T, t \) and \( x \) represent temperature, time and distance respectively; the subscript \( b \) denotes for blood. \( T_a \) and \( W_b \) are artillery temperature and blood perfusion rate respectively. \( Q_{\text{met}} \) and \( Q_{\text{ext}} \) are metabolic heat generation and external heat source in skin tissue respectively.

Considering Eq. (20) and replacing first order time derivative by Caputo fractional derivative of order \( \alpha \in (0, 1] \) and second order space derivative by Riesz–Feller fractional derivative of order \( \beta \in (1, 2] \). The fractional form of Pennes bioheat equation is given as

\[ \rho c \frac{\partial^\alpha T}{\partial t^\alpha} = k \frac{\partial^\beta T}{\partial x^\beta} + W_b c_b (T_a - T) + Q_{\text{met}}. \]  

(21)

Initial and boundary conditions of Eq. (21) are given below as

\[ T(x, 0) = T_a, \]  

(22)

\[ T(x, t)|_{x \to \pm \infty} = 0. \]  

(23)

To find solution of Eq. (21) to (23). We divide it into two parts, in first part, the time fractional is considered while in second part, the space fractional is considered.

**Time fractional bioheat equation**

On setting \( \beta = 2 \) in Eq. (21), this reduces to the following equation

\[ \rho c \frac{\partial^\alpha T}{\partial t^\alpha} = k \frac{\partial^2 T}{\partial x^2} + W_b c_b (T_a - T) + Q_{\text{met}}. \]  

(24)

For converting Eq. (24) in dimensionless variable, we consider

\[ \xi = \left( \frac{W_b c_b}{k} \right)^{\frac{1}{2}} x, \quad \eta = \left( \frac{W_b c_b}{\rho c} \right)^{\frac{1}{2}} t, \quad \theta = \frac{T - T_a}{T_0}, \quad \phi = \frac{Q_{\text{met}}}{T_0 W_b c_b}. \]  

(25)

On making the use of dimensionless variables as Eq. (25). We can reduce Eqs. (22) to (24) into Eq. (26) to (28) as

\[ \frac{\partial^\alpha \theta}{\partial \eta^\alpha} + \theta = \frac{\partial^2 \theta}{\partial \xi^2} + \phi, \]  

(26)

\[ \theta(\xi, 0) = 0, \]  

(27)

\[ \theta(\xi, \eta)|_{\xi \to \pm \infty} = 0. \]  

(28)

**Solution**

On replacing fractional derivative by Caputo fractional derivative and taking the Fourier–Laplace transform (Haubold et al. 2011b) of Eq. (26) and further using Eq. (5) and Eq. (6), we get
where $\theta^*$ is Fourier Laplace transform of $\theta$, on further simplifications, we get

$$
\bar{\theta}^*(\omega, s) = 2\pi \phi \delta(\omega) \frac{1}{1 + \omega^2} \left( \frac{1}{s} \right) - 2\pi \phi \delta(\omega) \frac{1}{1 + \omega^2} \sum_{m=0}^{\infty} (-1)^m \frac{s^{\alpha-1}}{(s^\alpha + \omega^2)^{m+1}}.
$$

(29)

On taking inverse Laplace transform of Eq. (29) and using Eq. (17), we get

$$
\theta^*(\omega, \eta) = 2\pi \phi \delta(\omega) \frac{1}{1 + \omega^2} \sum_{m=0}^{\infty} (-1)^m \eta^{\alpha m} \frac{m!}{m!} H_{1,1} \left( \frac{\eta \alpha}{1} \right) M_{1,2} \left( \frac{-m,1}{0,1,(-m,\alpha)} \right).
$$

(30)

On replacing derivative of Mittag-Leffler function by H-function using Eq. (19), Eq. (30) reduces to the following form

$$
\theta^*(\omega, \eta) = 2\pi \phi \delta(\omega) \frac{1}{1 + \omega^2} \sum_{m=0}^{\infty} (-1)^m \eta^{\alpha m} \frac{m!}{m!} H_{1,1} \left( \frac{\eta \alpha}{1} \right) M_{1,2} \left( \frac{-m,1}{0,1,(-m,\alpha)} \right).
$$

(31)

Now we consider

$$
G_m^*(\omega, \eta) = H_{1,1} \left( \frac{\eta \alpha}{1} \right) M_{1,2} \left( \frac{-m,1}{0,1,(-m,\alpha)} \right).
$$

(32)

to invert Fourier transform of Eq. (31), we first invert Fourier transform of Eq. (32), by taking its Mellin transform, since Mellin transform of H-function (Srivastava et al. 1982) is given below as

$$
M \left\{ H_{m,n}^{a,q} \left[ a \left( b_{ij}, b_{jk} \right) \right] \right\} (z) = a^{-z} \left\{ \prod_{j=1}^{m} \Gamma(1 - a_j - sA_j) \right\} \left\{ \prod_{j=1}^{n} \Gamma(1 - a_j - sA_j) \right\} \left\{ \prod_{j=m+1}^{n} \Gamma(1 - a_j + sA_j) \right\}.
$$

(33)

with the following conditions

$$
\delta = \sum_{j=1}^{q} \beta_j - \sum_{j=1}^{p} \alpha_j > 0,
$$

$$
A = \sum_{j=1}^{n} \alpha_j - \sum_{j=m+1}^{p} \alpha_j + \sum_{j=1}^{m} \beta_j - \sum_{j=m+1}^{q} \beta_j > 0, \quad |\arg(a)| < \frac{1}{2} A \pi,
$$

and

$$
-\min_{1 \leq j \leq m} \left( R \left( \frac{b_j}{\beta_j} \right) \right) < R(z) < \min_{1 \leq j \leq n} \left( R \left( \frac{1 - a_j}{\alpha_j} \right) \right).
$$

Further Mellin transform of a Fourier transform is given as (Langlands 2006)

$$
M[F[\psi(x)](q)](z) = 2\Gamma(z) \cos \left( \frac{\pi z}{2} \right) M[\psi(x)](1 - z),
$$

(34)
therefore the Mellin transform of Eq. (32) is

\[
M(G_m(\zeta, \eta))(x) = \left(\frac{1}{2}\right) \eta^{-\frac{x}{2}} \frac{\Gamma(\zeta) \Gamma\left(\frac{1}{2} + m - \frac{x}{2}\right) \Gamma\left(\frac{1}{2} + \frac{x}{2}\right)}{\Gamma\left(1 - \frac{x}{2} + \frac{\alpha x}{2}\right) \Gamma\left(\frac{1}{2} - \frac{x}{2}\right)}.
\]  
(35)

On taking the inverse Fourier transform of Eq. (31) by using Eq. (10), we get

\[
\theta(\zeta, \eta) = \phi \exp(-|\zeta|) - \phi \sum_{m=0}^{\infty} \left(-1\right)^{m} \frac{\eta^{em}}{m!} \int_{-\infty}^{\infty} \exp(-|\zeta|) \frac{1}{2\eta^{\alpha/2}} H_{2,1}^{1,2} \left[ \frac{1}{\eta^{\alpha/2}} \left| \zeta - \tau \right| \left(\frac{1}{2} - \frac{m}{2}\right), \left(\frac{1}{2}, \frac{1}{2}\right) \left(\frac{1}{2}, \frac{1}{2}\right) \right] d\tau.
\]  
(36)

**Special case**

On considering time fractional bioheat equation (24) in semi infinite space with \( Q_{net} = 0 (\phi = 0) \) and Neumann boundary condition on the left hand boundary, i.e. Eq. (23) is replaced by the following equation

\[
-k \frac{\partial T}{\partial x} \bigg|_{x=0} = q_0, \quad T(x, t) \bigg|_{x \to \infty} = 0,
\]  
(37)

for dimensionless variable, we consider

\[
\zeta = \left(\frac{Wbcb}{k}\right)^{\frac{1}{2}} x, \quad \eta = \left(\frac{Wbcb}{\rho c}\right)^{\frac{1}{2}} t, \quad \theta = \frac{T - T_a}{q_0 (kWbcb)^{\frac{1}{2}}}.
\]  
(38)

On making the use of Eq. (38), then Eqs. (24) and (37) reduce to

\[
\frac{\partial^{\alpha} \theta}{\partial \eta^{\alpha}} + \theta = \frac{\partial^2 \theta}{\partial \zeta^2},
\]  
(39)

\[
\frac{\partial \theta}{\partial \zeta} \bigg|_{\zeta=0} = -1 \quad \theta(\zeta, \eta) \bigg|_{\zeta \to \infty} = 0.
\]  
(40)

Further, on applying the Fourier cosine–Laplace transform to Eq. (39) and using Eq. (5) and Eq. (8), we obtain

\[
 s^\alpha \overline{\sigma}(\omega, s) - \theta(\zeta, 0) + \overline{\sigma}(\omega, s) = -\omega^2 \overline{\sigma}(\omega, s) + 1,
\]

where,

\[
 \overline{\sigma}(\omega, s) = F_{\zeta}[\theta(\zeta, \eta)] = \int_{0}^{\infty} \cos(\omega \zeta) \int_{0}^{\infty} e^{-s \eta} \theta(\zeta, \eta) d\zeta d\eta,
\]

further simplification leads us

\[
 \overline{\sigma}(\omega, s) = \sum_{m=0}^{\infty} \left(-1\right)^{m} \frac{1}{(s^\alpha + \omega^2)^{m+1}}.
\]  
(41)
Now taking inverse Laplace transformation to Eq. (41), as in light of Eq. (17), we get

\[ \theta^*(\omega, s) = \sum_{m=0}^{\infty} (-1)^m \frac{1}{\Gamma(m + 1)} \eta^{\alpha m + \alpha - 1} E_{\alpha,\alpha}^m (-\omega^2 \eta^\alpha). \]  

(42)

Afterwards using Eq. (19), then Eq. (42) reduces to the following form

\[ \theta^*(\omega, s) = \sum_{m=0}^{\infty} (-1)^m \frac{1}{\Gamma(m + 1)} \eta^{\alpha m + \alpha - 1} H_{1,2}^{1,1} \left[ -\omega^2 \eta^\alpha (-m,1)_{(0,1),(1-\alpha m,\alpha)} \right]. \]  

(43)

Now we find it’s inverse Fourier cosine transform by using Eq. (33) and the following result (Langlands 2006) as

\[ \frac{\sqrt{\pi}}{2} M[F_c[\psi(x)](q)](z) = \Gamma(z) \cos \left( \frac{\pi z}{2} \right) M[\psi(x)](1 - z). \]  

(44)

Thus we get

\[ \theta(\zeta, \eta) = \sum_{m=0}^{\infty} (-1)^m \frac{1}{\Gamma(m + 1)} \eta^{\alpha m + \alpha - 1} \frac{1}{(4\pi \eta^\alpha)^{1/2}} H_{2,3}^{2,1} \left[ -\frac{\left[ \zeta / (2,1),(\eta^\alpha/2,0,1),(1-\alpha/2,\alpha) \right]}{\eta^\alpha/2} \right]. \]  

(45)

This is the solution of special case for the time fractional bioheat equation in the form of well knows H-function (see in details Mathai et al. 2010).

**Space fractional bioheat equation**

we consider \( \alpha = 1 \) in Eq. (21) and dimensionless variables as

\[ \zeta = \left( \frac{W_b c_b}{k} \right)^{\frac{1}{2}} x, \quad \eta = \left( \frac{W_b c_b}{\rho c} \right) t, \quad \theta = \frac{T - T_a}{T_0}, \quad \phi = \frac{Q_{\text{met}}}{T_0 W_b c_b}, \]  

(46)

since Riez–Feller derivative of constant is not zero, therefore a new space dependent term \( f(\zeta) \) is introduced for simplification.

\[ \frac{\partial \theta}{\partial \eta} + \theta = \frac{\partial^\beta \theta}{\partial \zeta^\beta} + f(\zeta), \]  

(47)

where \( f(\zeta) = \frac{W_b c_b T_a}{\Gamma(1-\beta) \rho c T_0^\beta} \zeta^{-\beta} \), initial and boundary conditions are given in Eqs. (27) and (28) respectively.

**Solution**

On taking Fourier–Laplace transform of Eq. (47), and using Eq. (13), this leads us

\[ s \theta^*(\omega, s) - \theta(\zeta, 0) + \theta^*(\omega, s) = -|\omega|^\beta \theta^*(\omega, s) + f^*(\zeta) \frac{1}{s}, \]  

further simplification gives

\[ \theta^*(\omega, s) = f^*(\zeta) \frac{1}{1 + |\omega|^\beta} \left( \frac{1}{s} - \frac{1}{s + 1 + |\omega|^\beta} \right). \]  

(48)
On taking inverse Laplace transform of Eq. (47) and using Eq. (17), this yields

\[ \theta^*(\omega, \eta) = f^*(\xi) \frac{1}{1 + |\omega|^\beta} - f^*(\xi) E_{1,1}(-\eta) \frac{1}{1 + |\omega|^\beta} E_{1,1}(-|\omega|^\beta \eta), \]  

(49)

afterwards taking the inverse Fourier transform of Eq. (48) and employing the following results of Haubold et al. (2011b), which is given as

\[ F^{-1}\{E_{\beta,\gamma}(-\eta t^\beta |\omega|^{\alpha})\} = \left[ \frac{|\xi|}{\beta |\zeta|} \left( \frac{1}{(\eta^1/\beta)}(1,1/\beta,1,1/2) \right) \right], \]

\[ F^{-1}\{E_{1,1}(-\eta |\omega|^\beta)\} = \left[ \frac{|\xi|}{\beta |\zeta|} \left( \frac{1}{(\eta^1/\beta)}(1,1/\beta,1,1/2) \right) \right]. \]

(50)

Finally, we arrive at

\[ \theta(\omega, \eta) = \frac{1}{2\pi} F^{-1}\left\{ \sum_{k=-\infty}^{\infty} f(\zeta) \exp\left(-|\zeta|^2 \right) \right\} \]

\[ - E_{1,1}(-\eta) \frac{1}{2\pi} \int_{-\infty}^{\infty} f(\zeta) \exp\left(-|\zeta|^2 \right) \frac{1}{\beta |\zeta|} \left[ \zeta - \tau \right] \left[ \frac{1}{(\eta^1/\beta)}(1,1/\beta,1,1/2) \right] d\tau. \]

(51)

This is a solution of space fractional bioheat equation.

**Conclusion**

In this paper, we have investigated the temperature distribution of the biological tissue based on fractional bioheat transfer model. The fractional bioheat transfer equation is solved using integral transforms which yields analytical solution. This analytical solution may be useful in measurement of thermal parameters, reconstruction of temperature field, thermal diagnosis and thermal treatments.

**Authors’ contributions**

The authors contributed equally and significantly in writing this article. All authors read and approved the final manuscript.

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**Competing interests**

The authors declare that they have no competing interests.

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