Improving Surface Imprinting Effect by Reducing Nonspecific Adsorption on Non-Imprinted Polymer Films for 2,4-D Herbicide Sensors

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Abstract: Surface imprinting used for template recognition in nanocavities can be controlled and improved by surface morphological changes. Generally, the lithographic technique is used for surface patterning concerning sensing signal amplification in molecularly imprinted polymer (MIP) thin films. In this paper, we describe the effects of silanized silica molds on sensing the properties of MIP films. Porous imprinted poly(MAA–co–EGDMA) films were lithographically fabricated using silanized or non-treated normal silica replica molds to detect 2,4-dichlorophenoxyacetic acid (2,4-D) herbicide as the standard template. The silanized mold MIP film (st-MIP) (Δf = −1021 Hz) exhibited a better sensing response than the non-treated normal MIP (n-MIP) (Δf = −978 Hz) because the imprinting effects, which occurred via functional groups on the silica surface, could be reduced through silane modification. Particularly, two non-imprinted (NIP) films (st-NIP and n-NIP) exhibited significantly different sensing responses. The st-NIP (Δf st-NIP = −332 Hz) films exhibited lower Δf values than the n-NIP film (Δf n-NIP = −610 Hz) owing to the remarkably reduced functionality against nonspecific adsorption. This phenomenon led to different imprinting factor (IF) values for the two MIP films (IF st-MIP = 3.38 and IF st-MIP = 1.86), which was calculated from the adsorbed 2,4-D mass per poly(MAA–co–EGDMA) unit weight (i.e., QMIP/QNIP). Moreover, it was found that the st-MIP film had better selectivity than the n-MIP film based on the sensing response of analogous herbicide solutions. As a result, it was revealed that the patterned molds’ chemical surface modification, which controls the surface functionality of imprinted films during photopolymerization, plays a role in fabricating enhanced sensing properties in patterned MIP films.

Keywords: molecular imprinting; photopolymerization; silanization; hemispherical silica mold; herbicide

1. Introduction

The molecular imprinting technique is extensively used for various applications such as sorbents and sensors. Molecularly imprinted polymers (MIP) can be formed using this technique by undergoing a thermal/photopolymerization process between the monomers and the crosslinkers in the presence of target molecules to make mimicked cavities in the polymer matrix after template removal [1,2]. As a favorable sensing approach, molecular imprinting is widely employed as optical sensors [3], electrochemical biosensors [4], and biomimetic sensors [5,6] as well as is used for drug extraction applications [7].

Enormous effort has been invested into the development of MIP-based sensors, for example, for core–shell nanoparticles [8], lithographical patterns [9,10], and organic–inorganic...
hybrids [11]. Among them, the lithographic approach is an efficient tool for MIP structuring on sensing surfaces associated with quartz crystal microbalance (QCM) and could be combined with electro-/photochemical polymerization to fabricate specifically designed imprinted films. Various specific templates, from small molecules to large proteins, could be successfully imprinted on sensor platforms [12–16]. Recently, our group focused on increasing the sensing response of QCM-based MIP sensors by controlling the surface area of MIP films, which were fabricated using colloidal/soft lithography and photo-/electropolymerization [17]. Compared to their planar MIP film counterparts, the structured MIP films exhibited enhanced sensing signal response during a limited period owing to the increased surface area into which the specific template diffused in solution. The use of a poly(dimethylsiloxane) (PDMS) replica mold is a ubiquitous lithographic tool for generating MIP films during photopolymerization. However, pre-curing of the MIP precursor solution is required to prevent functional monomers, templates, and crosslinkers from being absorbed into the molds. Moreover, polystyrene (PS) or silica colloids can be used as a master mold to fabricate convex or concave hemispherical patterns [18]. Despite these lithographic approaches, the occurrence of undesirable nonspecific adsorption on non-imprinted polymer (NIP) thin films seriously affects the sensing parameters (i.e., the imprinting factor (IF) and the selectivity coefficient). In the past, we reported the adsorption of 2,4-dichlorophenoxyacetic (2,4-D) molecules on a template-extracted porous MIP thin films, which were lithographically fabricated using the silica colloidal array (d = 500 nm) as a master mold [19]. In that study, it was revealed that the hydroxyl groups on the surfaces of the silica colloids were involved in monomer–template complex formation during the polymerization process and increased nonspecific adsorption on the surface of the MIP/NIP films, consequently resulting in lowering the imprinting effect.

Thus, solving this problem in the lithographic process necessitates a new experimental strategy to control structural conformation on the surface of the MIP film formed in contact with patterned molds under photoirradiation.

Here, we report a simple strategy to decrease nonspecific binding on the surface of MIP/NIP films, leading to improved sensing properties. To this end, the surface of the structured silica particle arrays as a mold was modified with methylsilane and 2,4-D, which was used as a standard template to manipulate porous MIP thin films during the lithographic process. Fabrication of the porous MIP systems was conducted using methacrylic acid (MAA) as the functional monomer and ethylene glycol dimethacrylate (EGDMA) as the crosslinker via polymerization during microcontact lithography under ultraviolet (UV) exposure. Using a QCM, the sensing properties of the nanopatterned MIP films obtained from the silanized silica molds were measured in situ and compared to those of the MIP films that had been prepared with a non-surface-treated silica mold. Furthermore, the two corresponding NIP films were evaluated to identify differences resulting from the use of the two molds. Finally, other analogous herbicides were employed to investigate a change in selectivity of the two MIP films.

2. Materials and Methods

2.1. Materials

PS latex microspheres (d = 1 μm, 2.5 wt% dispersion in water) with a slight anionic charge were bought from Alfa Aesar Co., Ward Hill, MA, USA. Sodium dodecyl sulfate (SDS, Sigma–Aldrich Co., St. Louis, MO, USA) was used as an anionic surfactant to generate a robust PS colloidal monolayer. The SiO2 precursor was prepared using tetraethyl orthosilicate (TEOS, 98%, reagent grade) and absolute ethanol (99.5%, analytical reagent), which were purchased from Sigma–Aldrich Co. (St. Louis, MO, USA). Trimethoxy(methyl)silane (TMMS, Tokyo Chemical Industry Co., Tokyo, Japan) was used for methylation on the surface of SiO2. MAA, 2,4-D, and EGDMA were purchased from Tokyo Chemical Industry Co. (Tokyo, Japan) to be utilized as the functional monomer, template, and crosslinker, respectively. Dimethylformamide (DMF, ≥99%, Sigma–Aldrich Co., St. Louis, MO, USA) and 2,2′-azobisisobutyronitrile (AIBN, Daejung Chemicals & Metals Co. Ltd., Siheung,
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South Korea) were used as the solvent and photoinitiator, respectively. Other analogous chemicals such as atrazine (Sigma–Aldrich Co., St. Louis, MO, USA), ametryn (Sigma–Aldrich Co., St. Louis, MO, USA), and (4-chloro-2-methylphenoxy) acetic acid (MCPA, Tokyo Chemical Industry Co., Tokyo, Japan) were utilized for the selectivity test. Acetic acid and methanol were obtained from Duksan Co. Ltd., Ansan, South Korea. All other chemicals were used as received.

2.2. Close-Packed Arrangement of PS Microspheres

Close-packed PS microspheres were prepared on a glass substrate as per a previously reported technique [17]. Glass substrates were ultrasonicated for 5 min in acetone, ethanol, and DI water, sequentially, and dried under nitrogen (N$_2$) gas. Next, these substrates were immersed in a piranha mixture (H$_2$SO$_4$:H$_2$O$_2$, 3:1 v/v) for 40 min to remove all impurities. A small quantity of the PS dispersion (80 µL) was diffused on the cleaned substrate using a micropipette and spin-coated with 300 rpm for 5 min via a spin-coater (BGK, NSF-100DP). The randomly arranged PS microspheres on the substrate were floated carefully onto SDS assembled on an air/water interface in a Petri-dish. In this process, the PS microspheres were closely packed using an SDS aqueous solution of 200 µL (2 wt%). Finally, the monolayer was transferred onto the glass substrate ($\approx 2.5 \times 2.5$ cm$^2$) and allowed to dry completely for a day.

2.3. Porous Hexagonal-Patterned Polydimethylsiloxane (PDMS) Mold

A porous hexagonal-patterned PDMS mold was prepared using the PS colloidal monolayer as the sacrificial mask. First, the base elastomer (30 g) and 3 g of the Sylgard 184 curing agent (10:1 wt%, Dow Corning Co., Midland, MI, USA) were added to a glass bottle. After mixing for about ten mins, the air bubbles were removed using a DOA-P704-AC vacuum pump (Gast Manufacturing Inc., Benton Harbor, MI, USA). Next, the mixture was poured onto the colloidal mask in the plastic Petri-dish, and thermal curing was then performed at 60 $^\circ$C in an oven for 2.5 h. After removing the colloidal mask, the obtained PDMS mold was cut into pieces (2.0 cm $\times$ 1.5 cm) and rinsed with toluene for 5 min to remove the remaining microspheres.

2.4. Hemispherical SiO$_2$ Film

The hemispherical SiO$_2$ film was replicated in the reverse structure of the patterned PDMS mold. The SiO$_2$ precursor solution was prepared by sequentially placing TEOS (5.32 mL), absolute ethanol (9.5 mL), and HCl aqueous solution (0.1 N, 5 mL) in an N$_2$-filled glass bottle and stirring slightly for 1 h. After adding absolute ethanol (17.83 mL), the pre-hydrolyzed mixture was stirred again for 1 h before being stored at 5 $^\circ$C. The SiO$_2$ precursor (100 µL) was added dropwise onto the glass slide (2.5 cm $\times$ 2.5 cm). After covering the PDMS elastomer on the surface, thermal curing was conducted at 100 $^\circ$C on a hotplate for 1 h at 11.10 kPa. After peeling off the PDMS mold, the SiO$_2$ film was immersed in a mixture of TMMS (28.8 mL), absolute ethanol (25 mL), and HCl aqueous solution (0.1 N) for 4 h at room temperature to facilitate methylation on the surface for silane-treated replica molds (st-replica mold). The silanization step was omitted in non-treated replica molds (n-replica mold).

2.5. Porous Patterned MIP Film

MAA (0.4 mmol), 2,4-D (0.1 mmol), and EGDMA (2.0 mmol) were injected sequentially into a 5-mL vial. AIBN (0.05 mmol) was dissolved in DMF (50 µL) and added in the mixture solution. After purging with N$_2$ gas for 10 min, the MIP precursor (0.1 µL) was added dropwise to the SiO$_2$ film using a micropipette. Next, 9 MHz gold-coated AT-cut quartz crystal substrates (QCs, QA-A9M AU[M], 5 mm in diameter, Seiko EG&G, Seiko instruments Inc., Chiba, Japan) with an active gold area of 0.196 cm$^2$ was placed in contact with the SiO$_2$ film before being subjected to UV light (370 nm, 36 W) for 5 min. After photopolymerization (Figure 1), the QCs were gently peeled off the SiO$_2$ film. Finally, the
MIP film was immersed in a mixture consisting of methanol and acetic acid (9:1 v/v) for 30 min to extract the 2,4-D molecules in the polymer matrix. The NIP film was fabricated under the same procedures without the presence of 2,4-D.

![Diagram of molecular imprinted polymer (MIP) formation via photosynthetic reaction using a functional template, monomer, crosslinker, and initiator for 2,4-D molecular imprinting sensors.](image)

**Figure 1.** Molecular imprinted polymer (MIP) formation via photosynthetic reaction using a functional template, monomer, crosslinker, and initiator for 2,4-D molecular imprinting sensors.

Each MIP/NIP film was installed in a dip cell, and after the stabilization of resonant frequency in a few min, the frequency shift was measured in various 2,4-D solutions (from 40 to 100 nM) for sensitivity determination and in 100 nM of each herbicide solution (2,4-D, atrazine, ametryn, or MCPA) for selectivity analysis for a 2 h rebinding process using a QCA 922 quartz crystal analyzer (Seiko EG&G, Seiko instruments Inc., Chiba, Japan).

For the 9 MHz AT-cut gold-coated quartz crystals, the sensitivity factor was approximately 0.1834 Hz cm² ng⁻¹ [20]. A decrease of 1 Hz in the resonant frequency was almost identical to 1.07 ng in the mass loaded on the defined gold area. Thus, the mass of each imprinted polymer film (10–12 μg) was calculated from the resonant frequency differentiation of the bare and the 2,4-D-extracted imprinted quartz crystals oscillating in air. In addition, Q values (equilibrium binding capacities), denoted as the mass of the adsorbed 2,4-D molecules over the template-extracted poly(MAA–co–TFMAA–co–EGDMA) film were obtained from the Δf of each film in the sensing response.

### 2.6. Characteristics

The surface topographies of the MIP and NIP films were analyzed using field emission scanning electron microscopy (FE-SEM, Hitachi SU8220, Tokyo, Japan) and scanning probe microscopy (SPM, NX20, Park Systems, Suwon, South Korea).

### 3. Results and Discussion

As shown in Figure 2a, a convex hemispherical silica replica mold was manipulated using a pore-arrayed PDMS mold as a master mold, which was obtained from the PS colloidal monolayer, to form the porous patterned MIP/NIP films on gold-coated QC substrates. The well-ordered close-packed pattern in the silica observed in the SEM image had a small curvature of the hemispheres with a pore diameter of 830 nm and a pore height of 130 nm due to repeated executions of the replication process (Figure 2b). The atomic force microscopy (AFM) image was also obtained to determine a more accurate dimensional structure. The height (i.e., h at ≈90 nm) from the valley of the hemispheres was not precisely measured due to the AFM tip effect [21], but the hexagonal array of the silica was clearly observed (Figure 2c). For the porous MIP/NIP films, two silica replica molds (i.e., non-treated and silanized molds) were prepared to examine the differences in the nonspecific binding properties in the MIP/NIP films formed during the μ-contact printing process.
As shown in Figure 3a, the porous MIP/NIP film surface, which was in contact with the mold’s surface during photopolymerization, could be used as a sensitive interface for template detection; thus, the conformational control of this surface played an important role in determining the sensitivity of the QCM sensors. The MIP films (\( h_{\text{film}} \) at \( \approx 900 \text{ nm} \)) formed using the silanized silica molds (st-MIP) appeared to be thicker than those obtained from the silica colloidal arrayed molds previously reported [19], with an 800-nm pore diameter and a pore height of 125 nm, as determined via SEM and AFM surface analysis (Figure 3b). In addition, the surface-to-volume (S/N) ratio was estimated using surface statistics in the AFM analytical software to obtain an \( A/A_0 \) (i.e., surface area/geometric area) value of 1.096 (see Figure S1). In general, an increase in the surface area magnified the sensing signal relative to the planar MIP film’s signal due to a larger diffusion area during the limited sensing period [19]. In the absence of 2,4-D molecules, a non-imprinted polymer (NIP) film (st-NIP) was also prepared using the same procedure with a precursor solution to compare the sensing results with those obtained from the st-MIP film. As control samples, the MIP and NIP films were manipulated using non-silane treated silica molds to determine the effects exerted by the conformation structures of the imprinted films in the encapsulating process with two different molds on sensing properties. The surface morphology and geometrical dimensions of the st-NIP and MIP/NIP films were identical to those observed for the st-MIP film (see Figure S2).
used in the lithographically patterned MIP systems could inhibit nonspecific adsorption. was calculated based on the adsorbed 2,4-D mass per poly(MAA–co–EGDMA) unit weight (i.e., $Q_{\text{MIP}} / Q_{\text{NIP}}$) [22]. The st-MIP and n-MIP films had IF values of 3.38 and 1.86, respectively. This difference indicated that surface modification of the patterned molds used in the lithographically patterned MIP systems could inhibit nonspecific adsorption.
on the NIP films’ surface, thereby improving sensing properties. The molecular imprinting recognition on the porous MIP films, formed using st- and n-replica molds, is schematically represented in Figure 5.

![Figure 4](image1.png)

Figure 4. (a) Frequency change (Δf) on the n-MIP/NIP and st-MIP/NIP films as a function of time in a 100-nM 2,4-D aqueous solution for a 2-h rebinding process and (b) frequency change (Δf) as a function of 2,4-D’s concentration (from 40 to 100 nM).

![Figure 5](image2.png)

Figure 5. Expected molecular imprinting recognition on porous MIP films, obtained from surface imprinting using two replica molds: (a) st-replica mold and (b) n-replica mold.

As shown in Figure 4b and Figure S3, the Δf values were monitored in 2,4-D aqueous solutions with a concentration range between 40 and 100 nM to determine the sensitivity of the 2,4-D-detectable MIP films. Both the n-MIP and st-MIP films exhibited an increase in the Δf value with a corresponding increase in the concentration of 2,4-D. Additionally, the calibration curves were linear with coefficients of determination (R²) of 0.982 (n-MIP) and 0.949 (st-MIP), and the sensitivities obtained from the slope of linear fitting lines were ≈9.5 and 10.5 Hz/nM, respectively. Compared with the imprinted films, the n-NIP (4.8 Hz/nM) and st-NIP (3.5 Hz/nM) films showed significantly lower sensitivity. In particular, the st-NIP film retained the relatively low Δf value within the examined concentration range due to the small amount of nonspecifically bound 2,4-D molecules on the surface of the NIP film. Moreover, the Δf value of the n-NIP film was almost identical to that of the MIP film at the lowest concentration (40 nM), thereby confirming that this MIP system (IF ≈ 1.33) was not validated by the imprinting effect. However, the st-MIP film still had a high IF value of 2.40. Thus, surface modification protocols are required to enhance the sensing properties once a lithographic approach for fabricating the MIP system is applied. In addition, the MIP films were long-term stable and showed high reproducibility in sensing responses via several repeated measurements (n < 10).
As shown in Figure 6a, four herbicide molecules, including 2,4-D, were used for determining the specific selectivity, thereby verifying the efficiency of the 2,4-D-imprinted sensor. The Δf values of the n-MIP/NIP and st-MIP/NIP films were measured in herbicide solutions of 100 nM each for 2 h (Figure 6b and Figure S4). Both MIP films showed a similar sensing response to the 2,4-D molecule, but in the case of the st-MIP films, the sensing response was 45–100 Hz lower than that of the n-MIP film for the other herbicides. This was due to silanization of the used molds, which exerted influence on the surface conformation, regardless of the type of herbicide present. From the Q values described in Tables S1 and S2, we found that the sensing responses of the three similar herbicides on the st-MIP film ranged from 10.2 to 17.4 ng/μg. However, the n-MIP films exhibited a higher sensing response between 17.4 and 31.1 ng/μg due to increased nonspecific binding of the analogous herbicide molecules on the surface of the MIP film. From the Q values, we determined that the selectivity values (α = QMIP,2,4-D/QMIP,other herbicides) of the st-MIP and n-MIP films were within the ranges of 5.82–9.93 and 3.24–5.80, respectively. These results revealed that controlling the MIP films using silanized molds also contributed to the film’s selectivity. Similarly, in the case of the NIP films, the Δf value of the st-NIP film (250–335 Hz) was almost half-fold lower than that of the n-NIP film (480–570 Hz), regardless of the type of herbicide present.

Figure 6. (a) Chemical structures of the three herbicide molecules and 2,4-D, and (b) the Δf values of the n- and st-MIP/NIP films in each of the analogous herbicide solution (2,4-D, atrazine, (4-chloro-2-methylphenoxy) acetic acid (MCPA), or ametryn) with a fixed concentration (100 nM) for a 2-h rebinding process.

4. Conclusions

In summary, we lithographically fabricated porous MIP films (namely, st-MIP and n-MIP) by utilizing hexagonally close-packed hemispherical silica arrays (silanized or non-treated) as the mold to determine the effects of chemical surface modifications of the silica molds on the MIP sensing properties. As a standard template, the 2,4-D herbicide was used to establish sensitivity and selectivity. Compared to the n-MIP film, the st-MIP film showed improved sensing properties, such as an amplified frequency signal, better sensitivity, and higher selectivity, due to the restriction of unnecessary functionality. The MIP film that was made using the silanized mold (st-MIP) (Δf = −1021 Hz) exhibited noticeably better sensing responses than its MIP counterpart that was made using the non-treated normal (n-MIP) (Δf = −978 Hz). In particular, two NIP films (namely, st-NIP and n-NIP film) exhibited vastly different sensing responses during the nonspecific adsorption process, which was brought about by controlling the surface functionality of the st-MIP film. Moreover, it was revealed that the st-MIP film showed better selectivity than the n-MIP film. From these results, we learned that it was possible to control the surface functionality of the imprinted films during photopolymerization. In addition, the use of patterned molds...
with chemical surface modifications enhanced the sensing properties of lithographically patterned MIP films.

**Supplementary Materials:** The following are available online at https://www.mdpi.com/2227-9040/9/3/43/s1, Figure S1: Surface analysis of the st-MIP film, Figure S2: SEM and AFM images of st-NIP and n-MIP/NIP films, Figure S3: Frequency change as a function of time on the st-MIP/NIP and n-MIP/NIP films in a variety of 2,4-D concentrations, Figure S4: Frequency change as a function of time on the st-MIP/NIP and n-MIP/NIP films in each analogous herbicide solution, Table S1: Adsorbed mass, template-free polymer weight, and Qe values on the st-MIP/NIP and n-MIP/NIP films, Table S2: Selectivity coefficients ($k^*$) and relative coefficients ($k'$) of 2,4-D-imprinted and non-imprinted QCM sensors.

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**References**

1. BelBruno, J.J. Molecularly imprinted polymers. *Chem. Rev.* 2019, 119, 94–119. [CrossRef]
2. Chen, L.; Wang, X.; Lu, W.; Wu, X.; Li, J. Molecular imprinting: Perspectives and applications. *Chem. Soc. Rev.* 2016, 45, 2137–2211. [CrossRef]
3. Rico-Yuste, A.; Carrasco, S. Molecularly imprinted polymer-based hybrid materials for the development of optical sensors. *Polymers* 2019, 11, 1173. [CrossRef]
4. Gui, R.; Jin, H.; Guo, H.; Wang, Z. Recent advances and future prospects in molecularly imprinted polymers-based electrochemical biosensors. *Biosens. Bioelectron.* 2018, 100, 56–70. [CrossRef] [PubMed]
5. Ertürk, G.; Mattiasson, B. Molecular imprinting techniques used for the preparation of biosensors. *Sensors* 2017, 17, 288. [CrossRef]
6. Frasco, M.F.; Truta, L.A.A.N.A.; Sales, M.G.F.; Moreira, F.T.C. Imprinting technology in electrochemical biomimetic sensors. *Sensors* 2017, 17, 523. [CrossRef] [PubMed]
7. Madikizela, L.M.; Tavengwa, N.T.; Chimuka, L. Applications of molecularly imprinted polymers for solid-phase extraction of non-steroidal anti-inflammatory drugs and analgesics from environmental waters and biological samples. *J. Pharm. Biomed. Anal.* 2018, 147, 624–633. [CrossRef]
8. Xu, J.; Haupt, K.; Bui, B.T.S. Core–shell molecularly imprinted polymer nanoparticles as synthetic antibodies in a sandwich fluoroenzymoassay for trypsin determination in human serum. *ACS Appl. Mater. Interfaces* 2017, 9, 24476–24483. [CrossRef]
9. Lalo, H.; Ayela, C.; Dague, E.; Vieu, C.; Haupt, K. Nanopatterning molecularly imprinted polymers by soft lithography: A hierarchical approach. *Lab Chip* 2010, 10, 1316–1318. [CrossRef]
10. Tiu, B.D.B.; Pernites, R.B.; Tiu, S.B.; Advincula, R.C. Detection of aspartame via microsphere-patterned and molecularly imprinted polymer arrays. *Colloids Surf. A* 2016, 495, 149–158. [CrossRef]
11. Kla, S.; Fazilit, M.; Salavati, H.; Bohlooli, S. Preparation of a novel molecularly imprinted polymer by the sol–gel process for solid phase extraction of vitamin D3. *RSC Adv.* 2016, 6, 31906–31914. [CrossRef]
12. Guha, A.; Ahmad, O.S.; Guerreiro, A.; Karim, K.; Sandström, N.; Ostanin, V.P.; van der Wijngaart, W.; Piletsky, S.A.; Ghosh, S.K. Direct detection of small molecules using a nano-imprinted polymer receptor and a quartz crystal resonator driven at a fixed frequency and amplitude. *Biosen. Bioelectron.* 2020, 158, 112176. [CrossRef]
13. Cui, F.; Zhou, Z.; Zhou, H.S. Molecularly imprinted polymers and surface imprinted polymers based electrochemical biosensor for infectious diseases. *Sensors* 2020, 20, 996. [CrossRef]
14. Kalecki, J.; Iiskiero, Z.; Cieplak, M.; Sharma, P.S. Oriented immobilization of protein templates: A new trend in surface imprinting. *ACS Sens.* 2020, 5, 3710–3720. [CrossRef]
15. Chunta, S.; Boonsriwong, W.; Wattanasin, P.; Naklua, W.; Lieberzeit, P.A. Direct assessment of very-low-density lipoprotein by mass sensitive sensor with molecularly imprinted polymers. *Talanta* 2021, 221, 121549. [CrossRef] [PubMed]
16. Chunta, S.; Suedee, R.; Boonsriwong, W.; Lieberzeit, P.A. Biomimetic sensors targeting oxidized-low-density lipoprotein with molecularly imprinted polymers. *Anal. Chim. Acta* **2020**, *1116*, 27–35. [CrossRef]

17. Kong, S.; Yang, J.C.; Park, J.Y. Caffeine-imprinted conducting polymeric films with 2D hierarchical pore arrays prepared via colloidal mask-assisted electrochemical polymerization. *Sens. Actuators B* **2018**, *260*, 587–592. [CrossRef]

18. Park, J.Y. Effect of lithographically designed structures on the caffeine sensing properties of surface imprinted films. *Analyst* **2016**, *141*, 5709–5713. [CrossRef]

19. Aya, G.A.; Yang, J.C.; Hong, S.W.; Park, J.Y. Replicated pattern formation and recognition properties of 2,4-dichlorophenoxyacetic acid-imprinted polymers using colloidal silica array molds. *Polymers* **2019**, *11*, 1332. [CrossRef] [PubMed]

20. Donjuan-Medrano, A.L.; Montes-Rojas, A. Comparison of sensitivity constants of an electrochemical quartz crystal microbalance determined by potentiostatic deposition of Ti, Pb, Ag and Cu films. *Curr. Top. Electrochem.* **2012**, *17*, 75–85.

21. Flater, E.E.; Zacharakis-Jutz, G.E.; Dumba, B.G.; White, I.A.; Clifford, C.A. Towards easy and reliable AFM tip shape determination using blind tip reconstruction. *Ultramicroscopy* **2014**, *146*, 130–143. [CrossRef] [PubMed]

22. Gryshchenko, A.O.; Bottaro, C.S. Development of molecularly imprinted polymer in porous film format for binding of phenol and alkylphenols from water. *Int. J. Mol. Sci.* **2014**, *15*, 1338–1357. [CrossRef] [PubMed]