Clinical evaluations of mineralized collagen in the extraction sites preservation

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Abstract

The purpose of this study was to explore the different effects between biomimetic mineralized collagen (MC) and ordinary physically blended hydroxyapatite/collagen (HA/Col) composite in evaluating new bone formation and regenerated bone height in human extraction sockets. Thirty-four patients who cannot retain teeth caused by trauma or decay were randomly selected from Department of Stomatology of Dongzhimen Hospital from December 2013 to December 2014. The patients were randomly divided into two groups. After the operation of tooth extraction, 17 patients were implanted with biomimetic MC (MC group), and other 17 patients were implanted with ordinary physically blended nHA/Col composite (nHA/Col group). X-ray positioning projection by auto-photographing was taken to test the distance between the lowest position and the neighboring CEJm-CEJd immediately, 1 month and 3 months after the operation. The height of new bone formation of the MC group was significantly higher than the nHA/Col group. Biomimetic MC showed better clinical outcomes in the bone formation for extraction site preservation and would have broad application prospect in the field of oral and maxillofacial surgeries.

Keywords: mineralized collagen; biomimetic; extraction site preservation; bone formation height

Introduction

With the development of stomatology and material science, the rates of successful implanting supported denture are more and more higher, and these applications are widely accepted by more and more patients. At the same time, it is particularly necessary for an adequate of bone volume in the implant spot, because it is not only related to the success rate of implant surgery but also in terms of the aesthetic of gum soft tissue [1]. Clinicians prefer to conduct bone grafting at the time of tooth extraction for these patients who have an inadequate bone around the dental implant placement, thus can maximize to conserve bone volume and shorten the cycle of treatment.

Sites preservation [2] is a feasible method to solve the problem of lower bone level and long duration treatment, in which autologous bone, allogeneic bone or biological materials are placed in the extracted tooth socket following extraction. However, these materials have exhibited various shortcomings, such as the autologous bone from iliac bone has a satisfactory clinical effect and is regarded as a ‘gold standard’, but the source of autologous bones is limited, pain and infection in donor site are often associated with bone grafting. Also, allogeneic bone transplantation has some problems such as immunological rejection, cross infection of disease and ethical issues. So, tissue engineering expert researches were focused on the development of organic and/or inorganic compound. At present, internationally bone substitute...
materials researches focus on biological ceramic, polymer such as collagen (Col) and high molecular compound and hydroxyapatite (HA)/Col composite materials. But biological ceramic and polymer has some defects is difficult to meet the requirements of bone reconstruction and clinical applications. And mineralized collagen (MC) is the building blocks for various connective tissues such as bone, cartilage, tendon and dentin [3–5], therefore the research of nano-HA/Col (nHA/Col) composites which assemble organizational structure and function has become hot research area of artificial bone substitute materials [3, 6, 7].

Cui and co-workers [8] designed hierarchical self-assembly of MC nano-fibrils, which has natural bone like in terms of both the composition and the microstructure. The structure was consistent with the hierarchical structure of the self-assembled MC composite as described by Landis et al. [9], and the structure was demonstrated by conventional and high-resolution transmission electron microscopy for the first time [8]. Due to their biocompatibility, composition and structure are more similar to the natural bone, which in theory will be more popular and show more obvious advantages compared with the ordinary physically blended hydroxyapatite/Col (HA/Col) composite [10].

In this work, we explored the different effect between biomimetic MC and ordinary physically blended HA/Col composite result in evaluated new bone formation in human extraction sockets and bone height.

**Experimental**

**Materials**

The biomimetic MC implants were produced by Beijing Allgens Medical Science & Technology Co., Ltd. The implants were fabricated into extraction socket plug, which were easy to use by a dentist during the operation. The MC used in this study was hierarchical self-assembled nHA/Col composite, which has the same composition and microstructure with the nature bone and synthesized via an in vitro biomimetic mineralization process. As described by previously published literatures [8, 11], during the process of in vitro biomimetic mineralization, HA crystals grew on the surface of the Col fibrils with triple helices and their crystallographic c-axes oriented along the longitudinal axes of the fibrils to form MC fibrils. Then the MC fibrils aligned parallel to each other to form MC fibers. Such MC were collected and made into extraction socket plugs possessing a sponge-like structure with interconnected three-dimensional pores, Fig. 1b. As shown in Fig. 1a, the pore size was 100–400 μm, and the porosity was tested to be 90% [12]. These structures could provide sufficient space for cell adhesion, proliferation and osteoblast differentiation, which would accelerate the process of bone healing.

HA/Col bone graft material was provided by School of Materials Science and Engineering, Tsinghua University. The HA/Col material used in this study only has the same composition with the nature bone, the two component of hydroxyapatite and Col are physically blended and not biomimetic synthesis. Besides, its porosity is lower than the MC material.

**Method**

Patient selection: A total of 28 patients with 34 implants aged from 18 to 79 years were randomly selected from department of stomatology of Dongzhimen hospital from December 2013 to December 12, who cannot to retain the teeth caused by trauma or decay.

Accepting criteria: (i) All patients were systemically healthy, no tooth extraction contraindications; (ii) patients had intact four walls bone after tooth extraction and no bad granulation tissues in the extraction sockets and (iii) Patients were without active periodontitis and had a good oral hygiene.

These patients were randomly divided into two groups, group A was implanted with MC material and group B was implanted with HA/Col material. These patients should signature on the operation agreement and the experiment consent form before the operation.

Surgical procedures: Local mucosa was disinfected with Tincture of iodine and the periosteum of the tooth extraction sites was anesthetized with 3% Articaine; separated the gums from the teeth, loosened and extracted the teeth, curedt the extraction sockets and made sure that there is no bad granulation tissue in the socket and had intact four walls bone, the extraction sockets were grafted with MC material and HA/Col material randomly. The top of the gums were sutured 2–3 stitches with interrupted suture or 8-character-pattern to prevent the bone fillings fall out.

Evaluate the means: X-ray (SINORA HELIDENT Vario, Made in Germany) positioning projection by auto-photographing was taken to test the bone formation height, observe the speed and the quality of bone formation immediately, 1M and 3M after operation.

Measurement method: Take the connective line of the cemento-enamel junction of neighboring tooth on the mesial and distal sides (CEJM–CEJd) AB as the baseline, the lowest position on alveolar ridge defect as C point, and line of CD was perpendicular to the line of AB (Fig. 2). The distance of CD was measured at 1M and 3M after operation.
Statistical analysis: Using SPSS 18.0 statistical software for statistical analysis, distributions of variables were given as the mean and the standard deviation. The measurement data used variance test, counting card information using the test, the comparison of proportions using Fisher exact probability test. \( P < 0.05 \) represents the difference was statistically significant.

**Results**

We collected 28 patients with 34 implants in total. Group A included 13 patients with 17 implants, implanted with MC material produced by Beijing Allgens Medical Science & Technology Co., Ltd, group B included 15 patients with 17 implants, implanted with HA/Col material produced by School of Materials Science and Engineering, Tsinghua University. The accomplished cases of the two types of materials at different sites are listed in Table 1.

**The influence of the two types of materials on bone formation height**

The distance between the lowest position and the neighboring CEJm-CEJd was measured after the two types of materials were implanted into the tooth extraction sockets for 1 month and 3 months, the data are listed in Table 2. The height differences of group A is obviously higher than the control group B, which demonstrated that the bone formation height of group A was higher than group B in 1 month to 3 months. The data of the bone formation height of the two types of materials in site preservation were statistically analyzed in further, listed in Table 3.

For the factor of method, \( F = 15.62, P = 0.0004 < 0.05 \), the differences were statistically significant, which demonstrated that the MC material could be more effectively in preserving the height of alveolar bone than HA/Col material after tooth extractions. But for the method of time, \( F = 0.26, P = 0.6171 > 0.05 \), the differences did not achieve statistical significance, suggested that the MC material had no significant advantages at the same time after surgery.

![Figure 2. The measurement method of test and the distance between the lowest position and the neighboring CEJm-CEJd after operation](image)

**Table 1. Accomplished cases of the two types of materials at different sites and different sexes**

| Tooth position | Type A | Type B | Total |
|----------------|--------|--------|-------|
|                | M      | F      | M      | F      |-------|
| Front teeth    | 3      | 3      | 3      | 3      | 12    |
| Molar          | 3      | 3      | 3      | 3      | 12    |
| Premolar       | 3      | 2      | 2      | 3      | 10    |

**Table 2. The distance between the lowest position and the neighboring CEJm-CEJd of the two types of materials at different times (cm)**

| Object of observation (implantation site) | A 1M | A 3M | Height differences | B 1M | B 3M | Height differences |
|------------------------------------------|------|------|--------------------|------|------|--------------------|
| 1                                        | 1.51 | 1.35 | 0.16               | 2.36 | 2.73 | −0.37              |
| 2                                        | 0.62 | 0.34 | 0.28               | 1.76 | 1.70 | 0.06               |
| 3                                        | 1.81 | 1.73 | 0.08               | 2.25 | 2.54 | −0.29              |
| 4                                        | 1.93 | 1.08 | 0.85               | 2.59 | 2.68 | −0.09              |
| 5                                        | 1.93 | 0.62 | 1.31               | 1.86 | 2.23 | −0.37              |
| 6                                        | 0.57 | 0.61 | −0.04              | 2.07 | 2.32 | −0.25              |
| 7                                        | 2.16 | 2.00 | 0.16               | 2.39 | 2.45 | −0.06              |
| 8                                        | 3.00 | 2.97 | 0.03               | 1.96 | 2.02 | −0.06              |
| 9                                        | 0.98 | 0.32 | 0.66               | 2.98 | 2.72 | 0.26               |
| 10                                       | 1.00 | 0.81 | 0.19               | 1.75 | 1.53 | 0.22               |
| 11                                       | 1.56 | 1.02 | 0.54               | 2.38 | 2.65 | −0.27              |
| 12                                       | 1.35 | 1.25 | 0.1                | 1.55 | 1.82 | −0.27              |
| 13                                       | 0.69 | 0.45 | 0.24               | 1.07 | 1.55 | −0.48              |
| 14                                       | 1.68 | 1.35 | 0.33               | 1.05 | 1.54 | −0.49              |
| 15                                       | 1.87 | 1.54 | 0.33               | 1.37 | 1.81 | −0.44              |
| 16                                       | 2.00 | 1.88 | 0.12               | 1.87 | 1.94 | −0.07              |
| 17                                       | 1.69 | 1.46 | 0.23               | 2.16 | 2.62 | −0.46              |

\( t \pm s \) 0.33 ± 0.12 −0.20 ± 0.05
compared to the HA/Col material. Research on synthetical two factors method showed statistically significant, $F = 34.01 \ P < 0.0001$, the results illustrated that the longer time implanted the better osteogenesis effects obtained, the alveolar bone height 3 months after surgery was higher than 1 month after surgery when the same type of material implanted into the teeth extraction sockets, the results was accorded with the fundamental rules of bone remodeling of human.

Figure 3 exhibited two typical cases implanted with MC and HA/Col material. A, female, aged 64 years, implanted with MC material after removal of the mandibular left lateral incisor tooth and the mandible right lateral incisor tooth. B, female, aged 35 years, implanted with HA/Col material after removal of the maxillary right lateral incisor tooth. We can found that both new-bone formation height and density of case A were superior to case B at the same time by gross observation.

The speed of new bone formation of the two types of materials

The height and width of the new bone formation of some cases who are willing to dental implantation were measured by CT immediately and 3 months after surgery. Figure 4 shows a male aged 47 years implanted with MC material after removal of the mandibular right third molar. Spiral CT three-dimensional reconstruction and measurement of the height and width of new bone formation, each cases selected six point. The mean height and width of new bone formation at the 3rd month are $0.84 \pm 0.0046 \text{ mm}$ and $0.47 \pm 0.11 \text{ mm}$, respectively. Through statistics of the other four cases who were examined with CT, we found that the mean height and width of new bone formation who were implanted with MC were superior to those implanted with HA/Col material in general.

| Effect          | Num DF | Den DF | F Value | Pr > F |
|-----------------|--------|--------|---------|--------|
| Type            | 1      | 31     | 15.62   | 0.0004 |
| Time            | 1      | 31     | 0.26    | 0.6171 |
| Type*Time       | 1      | 31     | 34.01   | <.0001 |

The morphological change of the two types of materials at different time was further statistically analyzed, listed in Table 5. Chi-square = 0.9089, $P = 0.3404$, the difference between the two groups were not statistically significant. The contact interface of the two
groups became ambiguous from 1 month, so could be speculated that the time of morphological change is the start of new bone formation. The MC material had no advantage in speed of osteogenesis than the HA/Col material.

The speed of new bone formation of the two types of materials

The distance between the lowest position and the neighboring CEJm-CEJd was measured after the two types of materials implanted into the tooth extraction sockets 1 month and 3 months, the difference between different implanted sites and different sexes were compared. Data are listed in Table 6.

The results of the influence that materials implanted in different sites and different sexes to the osteogenesis effects were statistically analyzed as presented in Tables 7 and 8. The interaction of style and time is 0.000, below the 0.05 threshold, had statistical significance. All values of interactions in the last column are greater than 0.005, except Time*Type, and illustrated that the MC material is higher than HA/Col material in terms of new bone formation in 1–3 months but could not demonstrate that bone formation was related to the different implantation sites and sex.

Discussion

Healing of extraction sockets

Healing of extraction sockets is characterized by internal change and external change, the former manifest as lead to formation of bone within the socket and the latter manifest as lead to loss of alveolar ridge width and height [13]. So resorption and reconstruction of the external buccal and lingual socket walls result in a change in the dimensions of the ridge, this change may lead to the width and height of the alveolar ridge down and further affect the optimal implant aesthetics. The process of the healing of extraction sockets was first proposed by Steinhardt in 1932, and through the in-depth study

![Figure 4. Spiral CT three-dimensional reconstruction and measurement of the height and width of new bone formation for one case implanted with MC immediately and 3 months after surgery. (A) Three-dimensional reconstruction immediately after surgery. (B) Three-dimensional localization both horizontally and vertically. (C and D) The depth and width of teeth extraction socket immediately after surgery. (E and F) The depth and width of teeth extraction socket 3 months after surgery.](image-url)
experimental sites which covered with bioabsorbable membranes and vertical direction is 4.56 mm and 1.5 mm, respectively, but the tion, the average distance of bone resorption in horizontal direction that control sites without any membrane after 6 months of extrac-

bone basically completed around 3–6 months. The necessity of site preservation [18] is a measurement that is taken at the time of or following tooth extraction to prevent the alveolar ridge bone re-

of other scientists, the healing of extraction sockets can be divided into five stages [14]: The first stage, hemorrhage and formation blood clot: stop the bleeding within 15–30 min followed by formation of blood clot that fills the entire socket to prevent the infection of wound and promote wound healing; The second stage, the clot stimulates the granulation tissue formation: the gums begin to shrink within a few hours after extraction, vascular endothelial cells and fibroblasts begin proliferate after 24 h, the granulation tissue replaced the blood clot completely about 7 days. The third stage, the granulation tissue is replaced by connective tissue and epithelial tis-

sue: the connective tissue matures gradually within 5–8 days, the granulation tissue is replaced by connective tissue and epithelial tis-

ue: the alveolar process begin to reconstruct 3 days after extraction and gradually becomes mature bone tissue in 40 days, the remodeling of alveolar bone basically completed around 3–6 months. By way of 6 months clinical trial, Lekovic et al.[15,16] found that control sites without any membrane after 6 months of extrac-

tion, the average distance of bone resorption in horizontal direction and vertical direction is 4.56 mm and 1.5 mm, respectively, but the experimental sites which covered with bioabsorbable membranes presented with less horizontal resorption of the alveolar bone ridge. Schropp et al.[13] demonstrated that the major changes of an extrac-

tion site occurred during 1 year after tooth extraction, and two-thirds of the changes occurred in the first trimester. Araujo and Lindhe [17] have studied the dimensional changes of the alveolar ridge after tooth extraction and the processes of bone modeling and remodeling associated with this change. The results showed that the significant change occurred in the first 8 weeks, and during this period, there was a marked osteoclastic activity resulting in resorption of the buccal and the lingual bone wall. Because of the height of the walls at the buccal aspect of the extraction socket was significantly lower than the lingual aspect, the horizontal bone loss at the buccal aspect was more seriously than the lingual aspect.

It give us two enlightenment: (i) the effective intervence time of bone remodeling following tooth extraction is the first trimester and (ii) provided nature scaffolds for the osteoblast, which promote the cell migration and differentiation as well as bony union, and pre-

serve the bone mass of alveolar ridge in maximum.

The necessity of site preservation

Site preservation [18] is a measurement that is taken at the time of or following tooth extraction to prevent the alveolar ridge bone re-

sorption in maximum and provided sufficient alveolar bone volume and favorable ridge architecture for dental implantation. Indeed, any procedures can prevent the resorption of alveolar ridge can be seen as site preservation in broader understanding, such as choose the best time to undertake an extraction, minimally traumatic tooth extraction, soft and hard tissue grafting, concomitant use of barrier membranes and immediate implant placement [19]. Placing various bone graft materials inside the extraction socket is the most efforts

### Table 4. The comparison of the morphological change of the teeth extraction sockets with time

| Groups | 1M change | 1M no change | 3M change | 3M no change |
|--------|-----------|--------------|-----------|--------------|
| A      | 8         | 9            | 15        | 2            |
| B      | 5         | 12           | 14        | 3            |
| Total  | 13        | 21           | 29        | 5            |

### Table 5. The contrasting results of the time of morphological change of the teeth extraction sockets

| Statistic                      | Degree of freedom | Value   | Probability |
|--------------------------------|-------------------|---------|-------------|
| Chi-square                     | 1                 | 0.9089  | 0.3404      |
| Likelihood ratio chi-square    | 1                 | 0.9148  | 0.3389      |
| Continuous correction chi-square | 1              | 0.3361  | 0.5621      |
| Mantel-Haenszel chi-square     | 1                 | 0.8776  | 0.3489      |
| Phi coefficient                |                   | 0.1770  |             |
| Coefficient of association     |                   | 0.1743  |             |
| Cramer’s $\nu$                 |                   | 0.1770  |             |

### Table 6. The height differences in 1–3 months between the lowest position and the neighboring CEJm-CEjd after the two types of materials implanted in different sites, different sexes and different times (cm)

| Type            | Cases | Male Height differences | Cases | Female Height differences |
|-----------------|-------|-------------------------|-------|--------------------------|
| Front teeth     | A     | 0.23 ± 0.017            | 3     | 0.71 ± 0.47              |
|                 | B     | −0.2 ± 0.052            | 3     | −0.24 ± 0.019            |
| Molar           | A     | 0.28 ± 0.11             | 3     | 0.28 ± 0.054             |
|                 | B     | 0.047 ± 0.034           | 3     | −0.11 ± 0.080            |
| Premolar        | A     | 0.24 ± 0.0072           | 2     | 0.18 ± 0.0061            |
|                 | B     | −0.47 ± 0.0007          | 2     | −0.27 ± 0.076            |

### Table 7. The main effects and interactions of the repeated measure data of time variable

| Source | Type III sum of squares | DF | Mean square | $F$  | Sig |
|--------|-------------------------|----|-------------|------|-----|
| Time   | 0.051                   | 1  | 0.051       | 0.763| 0.392|
| Type* sex | 1.672                   | 1  | 1.672       | 24.877| 0.000|
| Type* sex | 0.055                   | 1  | 0.055       | 0.825| 0.373|
| Type* sex | 0.032                   | 2  | 0.016       | 0.240| 0.788|
| Type* sex* sex | 0.29                  | 1  | 0.029       | 0.429| 0.519|
| Type* sex* sex | 0.186                  | 2  | 0.093       | 1.382| 0.272|
| Type* sex* sex* sex | 0.300            | 2  | 0.150       | 2.235| 0.131|
| Type* sex* sex* sex* sex | 0.082        | 2  | 0.041       | 0.613| 0.551|
| Error (time) | 1.479                  | 22 | 0.067       |      |     |

### Table 8. The main effects and interactions of the other grouping factors

| Source | Type III sum of squares | DF | Mean square | $F$  | Sig |
|--------|-------------------------|----|-------------|------|-----|
| Intercept | 193.394                | 1  | 193.394     | 342.695| <.0001|
| Type | 8.667                   | 1  | 8.667       | 15.357| 0.001|
| Sex | 0.001                   | 1  | 0.001       | 0.002| 0.964|
| Position | 0.823               | 2  | 0.411       | 0.729| 0.494|
| Type* sex | 0.095                  | 1  | 0.095       | 0.168| 0.686|
| Type* position | 2.004             | 2  | 1.002       | 1.776| 0.193|
| Sex*position | 4.491              | 2  | 2.246       | 3.979| 0.033|
| Type*sex*position | 0.018           | 2  | 0.009       | 0.016| 0.984|
| Error | 12.415                  | 22 | 0.564       |      |     |
of current researches for this method is easy, little trauma and the materials have wide sources.

Site preservation can minimize external resorption of the alveolar ridge and maximize bone formation within the socket. Extensive clinical trials and animal experiments have demonstrated that placing various bone graft materials inside the extraction socket can prevent the height of alveolar ridge effectively in both height and width. Oltramari et al. [20] have demonstrated that treatment of postextraction alveoli with xenogenic grafting material can preserve bone height initially compared to when no xenograft is used are not sustained. Lasella et al. [21] found that the use of tetracycline-hydrated freeze-dried bone allograft in the fresh extraction sites lost less width and height and had more bone infill compared to the test group of natural healing. Mardas et al. [22] used a synthetic bone substitute and a bovine-derived xenograft combined with a Col membrane to preserve the alveolar ridge dimensions following tooth extraction, the width of the alveolar ridge reduce by 13% and 23%, respectively, and both of them are significantly lower than the control group of natural healing.

From histological perspective, site preservation techniques following tooth extraction can provide good bone for dental implant. Though many literature have demonstrated that the extraction sockets can form to new bone by site preservation techniques, there are many different between the speed and quantity of new bone formation, which related to the biological and physical and chemical properties of the materials that selected closely. Thus, we put forward a higher requirement to the bone graft for site preservation.

**Bone graft materials**

An ideal bone-grafting material should not only have a good biocompatibility and biodegradability but also be able to produce bone by osteogenesis, osteoinduction and osteoconduction [23]. Besides, their mechanical properties should be equivalent to or better than those of natural bone [24]. Thus, autogenous bone is regarded as a ‘golden standard’ because it is biocompatible and has the potential to form new bone through osteogenesis, osteoinduction and osteoconduction, but its application is limited by the amount of source and post-operative discomfort of the donor site [25]. Several types of bone substitutes are commercially available in recent years, such as allograft, xenografts and alloplasts. They all have some disadvantages, allograft and xenografts cannot avoid the risk of disease transmission, immunological rejection and ethical issues; alloplasts are synthetic bone substitutes that act as a biologic filler with limited periodontal regeneration when used in treating periodontal bone defects [26].

Therefore, based on the understanding of the natural bone and its formation process, many studies have been performed to prepare biomimetic materials mimicking the native bone in the composition, microstructure and the processes of mineralization [27–29]. Designing and preparing new materials and synthesizing bone substitute materials mimicking the natural bone have become a hot topic in the field of biomaterials [30]. Although many scholars have obtained the so-called ‘mineralized collagen’ that consisted of Col/HA composites with or without the self-assembly structure of the natural bone MC, some of them are not strictly a bionic technology. And some of them [31–36] are lack of evidence demonstrating the presence of self-assembled MC and orderly arranged nano-sized HA crystals within the Col fibrils. Cui and co-workers [8, 10] designed MC nano-fibrils via hierarchical self-assembly, which were consistent with autologous bone in terms of both the composition and the microstructure. For the first time, the hierarchical self-assembly structure of Col/HA composite was verified by conventional and high-resolution transmission electron microscopy [8]. This study has gained widespread international attention in the field of biomaterials, and Nature Materials commented and posted a literature noted that ‘The authors found that nanocrystals of the minerals were deposited along the surface of the fibrils—giving the first direct evidence to support previous theories that this occurs’ [37].

**Conclusions**

The two types of materials used in this study have the same composition of HA and Col but have different microstructures. Compared to physically blended nHA/Col, biomimetic MC had significant promotion effect on the height of bone formation. Therefore, the microstructure played an important role in clinical performance for the bone grafts. The MC with biomimetic composition and microstructure would have broad clinical application prospect in the field of oral and maxillofacial surgeries.

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**Conflict of interest statement.** None declared.

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