Acute Physiological Response of Lumbar Intervertebral Discs to High-load Deadlift Exercise

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Purpose: We aimed to evaluate the acute physiological effects of high-load deadlift exercise on the lumbar intervertebral discs using MR diffusion-weighted imaging (DWI).

Methods: Fifteen volunteers (11 men and 4 women; 23.2 ± 3.3 years) without lumbar intervertebral disc degeneration performed deadlift exercise (70% of 1 repetition maximum, 6 repetitions, 5 sets, 90 s rest between sets) using a Smith machine. Sagittal MR diffusion-weighted images of the lumbar intervertebral discs were obtained using a 1.5-Tesla MR system with a spine coil before and immediately after the exercise. We calculated apparent diffusion coefficient (ADC; an index of water movement) of the nucleus pulposus from diffusion weighted images at all lumbar intervertebral discs (L1/2 through L5/S1).

Results: All lumbar intervertebral discs showed significantly decreased ADC values immediately after deadlift exercise (L1/2, −2.8%; L2/3, −2.1%; L3/4, −2.8%; L4/5, −4.9%; L5/S1, −6.2%; P < 0.01). In addition, the rate of ADC decrease of the L5/S1 disc was significantly greater than those of the L1/2 (P = 0.017), L2/3 (P < 0.01), and L3/4 (P = 0.02) discs.

Conclusion: The movement of water molecules within the lumbar intervertebral discs is suppressed by high-load deadlift exercise, which would be attributed to mechanical stress on the lumbar intervertebral discs during deadlift exercise. In particular, the L5/S1 disc is subjected to greater mechanical stress than the other lumbar intervertebral discs.

Keywords: magnetic resonance diffusion-weighted image, intradiscal water movement, lumbar spine, lifting, mechanical stress

Introduction

A deadlift is a popular exercise that is frequently incorporated into athletic training programs. This exercise is effective in strengthening the back and lower extremity muscles, but the lumbar spine is subject to mechanical stress such as shear and compression forces during deadlift.1–4 The stress is expected to become greater with increasing exercise weight. Therefore, the lumbar region is most susceptible to injury during high-load deadlift.5,6 In addition, the repeated lifting of heavy weights has been identified as a risk factor for lumbar intervertebral disc degeneration/herniation.3 The lumbar intervertebral discs are thought to gradually degenerate through high-load deadlift training. However, to the best of our knowledge, little is known about the acute physiological changes of the lumbar intervertebral discs resulting from high-load deadlift exercise.

MRI has been used as a noninvasive method to investigate the status of the intervertebral discs in both clinical and experimental settings. In particular, diffusion-weighted imaging (DWI) can quantitatively evaluate the movement of water molecules (water diffusion) within the intervertebral disc by calculating an apparent diffusion coefficient (ADC). The intradiscal water movement is partially associated with intervertebral disc composition. Degenerated intervertebral discs show significantly lower ADC values than normal discs mainly due to reduced absolute intradiscal water content.7–10 In addition, the intradiscal water movement is sensitive to mechanical stress placed on the intervertebral disc. It was confirmed using ovine lumbar intervertebral discs11 or cadaveric human lumbar intervertebral discs12 that the ADC value of the lumbar intervertebral disc decreases under compressive loads. Thus,
the ADC value is thought to be a useful parameter for noninvasively evaluating the acute stress responses of the lumbar intervertebral discs to high-load deadlift exercise.

The purpose of this study was to investigate the acute physiological effects of high-load deadlift exercise on the lumbar intervertebral discs using MR DWI. The findings of this study would help to deepen our understanding of the mechanism by which the repeated lifting of heavy weights leads to lumbar intervertebral disc degeneration/herniation. We expected that the water movement within the lumbar intervertebral discs would decrease after high-load deadlift exercise as an acute stress response to repetitive mechanical stress.

Materials and Methods

Subjects
A total of 15 healthy volunteers (11 men and 4 women; mean age, 23.2 ± 3.3 years; age range, 19–30 years) with normal lumbar intervertebral discs participated in this study. The state of the lumbar intervertebral discs was assessed a few days before the measurement, according to the Pfirrmann scale for disc degeneration based on the signal intensity (SI) on a midsagittal T2-weighted MR image. Those with bulging, degenerated, and/or herniated discs were not included in this study. All of the participants were not regularly engaged in any sports activities at the time of measurement. No participants reported any pain and discomfort at the time of measurement and there was no previous history of surgery or injury in the lumbar region or lower extremities. Participants were instructed to refrain from any physical exercise beginning 48 h prior to the measurement.

This study was approved by the ethical committee of Waseda University and followed the ethical guidelines of the Declaration of Helsinki. Prior to the measurement, all participants were given a brief description of the study, the examination procedures, and the potential risks. Written informed consent was obtained from each participant.

Deadlift
After pre-exercise MRI measurements of the lumbar intervertebral discs, the participants performed a non-standardized warm-up including self-stretching and submaximal deadlift repetitions. The deadlift was performed without a weight belt using a Smith machine (Nautilus, Vancouver, WA, USA) (Fig. 1). The participants stood near the bar with a shoulder width stance on a stool placed in the Smith machine and squatted down to grasp the bar with an alternated grip, slightly wider than shoulder width with the arms straight and the hips lower than the shoulders. From the start position, they lifted a weight corresponding to 70% (69.2 ± 18.7 kg) of their 1 repetition maximum by extending the hips and knees and keeping the posture of the spinal column in a neutral position (a straight back), until a fully erect body position was established. Then, they lowered the bar maintaining the neutral spinal position. We instructed them to lift and lower the bar as near to the body as possible. Verbal feedback regarding their deadlift technique was provided during the exercise. Each repetition was performed in a controlled manner by using a metronome with 2 s lifting and lowering phases. This 4 count action was repeated for 5 sets of 6 repetitions with a 90 s interval between sets, for a total of 30 repetitions.

MR imaging
Midsagittal DW images of the lumbar intervertebral discs were obtained in a supine position before and immediately after pre-exercise MRI measurements.

Fig. 1 The start (a) and finish (b) positions of high-load deadlift exercise. The participants lifted and lowered a weight corresponding to 70% of their 1 repetition maximum using a Smith machine.
after the deadlift exercise using a 1.5-Tesla MR system (Signa HDxt, GE Healthcare UK, Little Chalfont, Buckinghamshire, England) with a spine coil at Waseda University. We could start the scan of a post-exercise DW image within 5 min after deadlift exercise because the exercise was performed near a MRI room. The DWI sequence (spin-echo type single-shot echo-planar imaging without parallel imaging) was as follows: TR, 6000 ms; TE, 76.4 ms; 256 × 256 matrix; number of excitations, 4; field of view (FOV), 300 mm; rectangular (phase) FOV, 0.5; slice thickness, 10 mm; b-value, 500 s/mm²; acquisition time, 1 min 42 s; and water excitation of a single slice. The choice of a rectangular FOV minimized geometric distortions from susceptibility differences. We applied a motion-probing gradient with a b-value of 500 s/mm² sequentially in each of three main orthogonal orientations (x-, y-, and z-axes). DW image acquisition produced one baseline echo-planar T₂-weighted image (b-value, 0 s/mm²) without a motion-probing gradient and one isotropic DW image (b-value, 500 s/mm²) that was generated by averaging the ADC value from each DW image in the three orthogonal orientations.

To calculate the ADC values of 5 lumbar intervertebral discs (L1/2 through L5/S1) before and immediately after the exercise, we constructed pre- and post-exercise ADC maps using the FuncTool 2 software program (GE Healthcare UK) built into the MR device. We obtained the ADC map using one baseline echo-planar T₂-weighted image and one isotropic DW image (b-value, 500 s/mm²) without a motion-probing gradient. The intensity of the pixels on the map corresponded to the absolute ADC values of tissue. A ROI was drawn so that it completely surrounded the nucleus pulposus of each lumbar intervertebral disc on the echo planar T₂-weighted image. The ROI was then copied to the ADC map. The ADC value of the nucleus pulposus was calculated using the equation: ADC = ln(SI/SI_b000) / (b000 − b0), where SI is the SI in the ROI without a motion-probing gradient (b-value, 0 s/mm²; b0), and SI_b000 is the SI in the ROI with a b-value of 500 s/mm² (b500). In addition, the percentage change in ADC value post-exercise was defined as a % change in ADC value = (post-exercise ADC value − pre-exercise ADC value) / pre-exercise ADC value × 100.

**Statistical analysis**

We calculated the mean and standard deviations for pre- and post-exercise ADC values, and the percentage change in ADC values of five lumbar intervertebral discs. The Shapiro–Wilk test was used to check for normal distributions of all ADC values. Then, the ADC values of 5 lumbar intervertebral discs were compared before and after the deadlift exercise using a paired t-test. In addition, significant differences between the percentage changes in ADC values of five lumbar intervertebral discs were evaluated by one-way analysis of variance with a Tukey’s post-hoc test. Moreover, effect sizes (Cohen’s d) were calculated and evaluated as trivial (0–0.19), small (0.20–0.49), medium (0.50–0.79), and large (0.80 and greater). Statistical analysis was performed using SPSS Statistics 23 software (IBM, Armonk, NY, USA). Statistical significance was set at P < 0.05.

**Results**

Table 1 displays the ADC values of five lumbar intervertebral discs before and immediately after high-load deadlift exercise. All lumbar intervertebral discs showed significantly decreased ADC values after the exercise (P < 0.01). In addition, ADC decrease of the L5/S1 disc was significantly greater than those of the L1/2 (P = 0.017), L2/3 (P < 0.01), and L3/4 (P = 0.02) discs (Fig. 2). Figure 3 shows the decreased ADC value of the L5/S1 disc on an ADC map after high-load deadlift exercise for a representative subject.

![Fig 2](image-url)  
**Fig. 2** The percentage change in the apparent diffusion coefficient values of 5 lumbar intervertebral discs before and immediately after high-load deadlift exercise.
Discussion

In the present study, all 5 lumbar intervertebral discs showed significantly decreased ADC values after high-load deadlift exercise. ADC value reflects both the water diffusion and capillary perfusion within tissues. However, the effect of perfusion is thought to be negligible in the intervertebral discs because of their avascularity, although we used relatively low $b$-value (500 s/mm$^2$). Thus, the findings of this study imply that repeated lifting of heavy weights decreased the movement of water molecules within the nucleus pulposus of each lumbar intervertebral disc. Intradiscal water movement is suppressed by applying compression force to the lumbar intervertebral disc. Eltoukhy et al. calculated, using a biomechanical spine model based on motion capturing, that the lumbar vertebrae are subject to axial compressive force (6488–7963N), shear force (1220–1903N), and bending moment (685–747 Nm) during the deadlift with a weight corresponding to approximately 75% of the one repetition maximum. They also found that the axial compressive force reaches a maximum at up-right standing position during the deadlift. Thus, we infer that the decreased ADC values reflect repetitive mechanical stress on the lumbar intervertebral discs that occurred during high-load deadlift exercise.

In addition, the present study revealed that the L5/S1 disc shows a significantly greater ADC decrease than the L1/2, L2/3, and L3/4 discs after high-load deadlift exercise. This finding suggests that the L5/S1 disc are more subject to mechanical stress resulting from high-load deadlift exercise among the lumbar intervertebral discs. Eltoukhy et al. reported that maximum compressive and shear forces occurred at the L5 vertebra during high-load deadlift. Thus, larger mechanical forces might occur at the L5/S1 disc during high-load deadlift exercise in the present study. Considering that the L5/S1 disc is a high incidence site of lumbar intervertebral degeneration/herniation, special clinically attention should be paid to this region during high-load exercise to prevent lumbar injuries.

Degenerated intervertebral discs show significantly lower ADC values than normal discs. The decreased ADC values would be associated with losses of water and/or proteoglycan contents in the nucleus pulposus. It is likely that repetitive mechanical stress gradually changes the composition of the intervertebral disc, resulting in intervertebral disc degeneration. In the present study, acute ADC decreases as a result of high-load deadlift exercise were relatively small, but the accumulation of the small responses may lead to lumbar intervertebral disc degeneration. Furthermore, although the findings of the present study do not imply that the lumbar intervertebral discs will necessarily be degenerated by repetitively performing high-load deadlifts, we hope that these findings will contribute to a better understanding of the mechanisms of lumbar injuries during deadlift exercise.
There are some limitations in the present study. First, since we only performed MRI measurements before and immediately after the deadlift exercise, the recovery time of decreased ADC values remains unclear. Second, the participants could not completely keep the bar in contact with their body during the deadlift by using the Smith machine. Thus, it is possible that the flexion moment at the lumbar spine became greater than what would have occurred in a free-weight deadlift where the bar is kept close to the body throughout, resulting in greater mechanical stress on the lumbar intervertebral discs when using the Smith machine. Third, although we evaluated the status of the lumbar intervertebral discs in a midsagittal image, additional axial images might provide useful physiological information on the intervertebral discs. However, the number of post-exercise measurements should be limited to adequately identify the acute responses of the tissues to exercise. Finally, although we did not measure the sagittal alignment of the lumbar spine before exercise, it might influence on the magnitude of mechanical stress on the lumbar intervertebral discs during deadlift exercise.  

**Conclusion**

High-load deadlift exercise places mechanical stress on all of the lumbar intervertebral discs. In particular, the L5/S1 disc is subjected to greater mechanical stress compared with the upper lumbar discs during high-load deadlift exercise.

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**Conflicts of Interest**

We have no conflicts of interest to declare.

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