Analysis by Computer Simulation of Factors Affecting the Extracellular Slow Wave Features of the Human Colon

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Abstract: The study reported in this paper analyses, by computer simulation, factors affecting the features (amplitude, frequency and phase lag) of the slow waves of the extracellular myoelectrical activity of the human ascending colon. It takes into account both the anatomic and functional aspects of the colon haustra, the myoelectrical dynamics of the cells and the geometric modification of haustra’s configuration. The variable sacculated geometry of the colon wall, segmented into typical haustra, has been represented by a sequence of truncated round ellipsoids. According to the propagation of the front of depolarization-repolarization of the cells, slow waves are simulated by the cyclic movement of an annular band polarized by electrical dipoles oriented perpendicularly with respect to the surface of the ellipsoids and activated by a pacemaker. The simulation highlighted that the amplitude of the slow waves physiologically depends on the dipole moment of cells, and the frequency depends on the velocity of the polarized annular band. In addition, the amplitude, the frequency and the phase lag also depend on the dynamic modification of the geometrical factors (colon length and haustrum radius). Furthermore, the simulation results showed that the shape of the slow wave and the amplitude of its peaks depend on the inter-electrode distance and on the electrode positioning with respect to the lower edge of ellipsoids.

Keywords: Computer Simulation, Extracellular Myoelectrical Activity, Human Colon

1. Introduction

The human colon is a sacculated organ composed by a set of haustra brook apart by semilunar folds that retain digesta [1]. The structure with haustra and folds allows to obtain a considerable change in the internal volume of the organ with a relatively little contractions of the musculature, i.d. small changes of the surface area carry out an effective type of regulation of the digesta transit through the tract [1]. The human colon has a thick circular muscle coat arranged in loosely packed bundles and is covered with a continuous thin coat composed by longitudinal muscular cells that thickens in three regions called taeniae coli. Contractile activities of the smooth muscle are regulated to produce the storage, the mechanical and chemical decomposition, and the transport of digesta. During the transport of digesta, muscles are stimulated to contract pushing the contents to the next haustrum. One of the control systems that regulates the chemical and mechanical actions that accomplish the digestive process is the myogenic control system involving the electrical activity of the membrane of the smooth muscle cells [2]. While much is known about the mechanism underlying the origin and the regulation of the electrical activity of the stomach [3], such mechanisms are still poorly known regarding to the human colon. Most of our knowledge regarding the electrophysiology of the colon derives from experiments made on animals, such as the pig, the dog and the cat [4-7]. Studies on the cat colon [4] suggested that circular smooth muscle layer is the site of origin and propagation of electrical slow waves. Studies on the canine colon electrophysiology identified the cells that activate the electrical slow waves [5]. Now it is known that the interstitial cells of Cajal, organized as a network of specialized cells, are the pacemaker of the gastrointestinal electrical activity [8-9]. The available literature related to the understandings of the myoelectrical activity of the human colon, as recorded with in vivo measurements, is not recent as it is no longer possible to perform in vivo experiments on human beings. The main characteristics of the slow waves of the human colon, as recorded with implanted bipolar electrodes [10-17], revealed that the slow waves of the ascending colon were highly
irregular and time varying. In details, Sarna et al. [10-11] stated that in the ascending colon the dominant frequency component was in the range of 2.0–9 cpm with a mean value equal to 4.57 cpm; the signal level was in the range 0.1 – 0.5 mV/cm; waveforms picked up with adjacent electrodes were not phase locked. Condon et al. [12] stated that in ascending colon the slow waves are omnipresent and have three ranges of frequency: from 2.7±0.1 cpm to 4.3±0.2 cpm, from 10.09±0.2 cpm to 11.5±0.1 cpm, and from 25.5±2.3 cpm to 32.6±2.3 cpm. Taylor et al. [13] reported that the slow wave activity of the human colon is not present at all times and that two rhythms are present, a predominantly higher one at 6 to 12 cycles/min and one at a lower frequency at 2 to 4 cycles/min. However, little has been done to investigate the possible reasons for these irregularities.

The modeling approach can be useful to investigate, by simulation, the myoelectrical activity of the human colon and to analyze the factors affecting the extracellular slow waves. While many theoretical models have been developed for the slow wave of the human stomach and gastrointestinal tract [18-27], few have been developed for the slow wave of the colon [28-31]. First models to simulate the colonic slow waves were based on the relaxation oscillators that do not refer to the anatomy and physiology of the organ [28,29]. The basic modeling approach proposed here is based on the electric dipole model we used to simulate slow waves of the human stomach [20,21] and the cat colon [30-31]. This approach has proved to be useful in reproducing the characteristics of both the slow waves and the burst activity [21, 30]. The mathematical model was developed taking into account the geometrical characteristics of the human colon and the myoelectrical dynamics of cells. The ascending tract of the colon was taken into account.

The aim of this study was to analyze, by computer simulation, whether changes in the physiological factors (dipole moment and velocity of depolarization-polarization of cells) and in the geometrical factors (colon length and hastrum radius) may change the features (amplitude, frequency and phase lag) of slow waves as obtained with implanted bipolar electrodes. Furthermore, the effects on peaks’ amplitude due to the inter-electrode distance and to the electrode positioning with respect to the lower edge of the ellipsoids were analyzed.

2. Material and Methods

2.1. The Basics of the Model

The development of model takes into account the following conditions:

- the hastrum wall was considered composed only by the circular muscle coat since it is the site where electrodes were implanted to record the slow waves with in vivo and in vitro experiments [4-6];
- the smooth muscle layer was considered as homogeneous. Its electrical permittivity is \( \varepsilon = \varepsilon_0 \varepsilon_r \); \( \varepsilon_0 \) is the electrical permittivity in free space; Appendix C of [32] reports the diagrams showing the value of the relative electrical permittivity \( \varepsilon_r \), and other properties of many body tissue in the frequency range 1.0E+1 to 1.0E+11 Hz;
- the colon hastrum were represented by a set of truncated ellipsoids obtained by rotating a truncated ellipses (Figure 1);
- cells were represented by electric dipoles since they have a resting membrane potential due to a balanced ionic distribution across the cells’ membrane. The pacemaker potential generated by the interstitial cells of Cajal [33,34] upsets the balance and causes the inversion of polarity across the cells’ membrane by a periodic membrane depolarization;
- the cells of the smooth muscle that, at a given instant, give rise to the membrane depolarization were spread in an annular band, \( \delta \)-wide polarized by electric dipole perpendicularly oriented to the surface of the ellipsoid (Figure 1);
- the distribution of the dipoles in the remaining part of the ellipsoids was considered as random so that it...
generated a null potential in each and every point of space;

• the dipole density \( \mathbf{D} \) of the polarized annular band was taken as constant. The dipole moment of the infinitesimal area \( dS \) is \( \mathbf{p} = \mathbf{D} dS \);

• since the depolarization activated by the cells of Cajal, after its initiation, propagates as a wave into the adjacent muscle layers [33,34], we considered that slow waves were generated by the periodic movement of the polarized annular band, \( \delta \)-wide in the aborad direction from the bottom to the top of the ellipsoids (peristaltic movements).

For a segment of length \( l_c \), the velocity \( v \) to obtain the frequency \( f \) (measured in Hertz) was determined by the following relationship:

\[
v = l_c \cdot f
\]

\[
f(z, \Theta, \psi) = \frac{\{R_{xy}(z_p - z) \cos \psi - \left[R_{xy}^2 - R_{xy}p_{xy} \cos(\Theta - \psi)\right] \sin \psi\}}{\left[R_{xy}^2 + z^2 + \rho_{xy}^2 + z_p^2 - 2 \left[z_p + R_{xy}p_{xy} \cos(\Theta - \psi)\right]\right]^{1/2} \left[R_{xy}^2 + z^2\right]^{1/2}}
\]

So for \( V(\mathbf{f}, t) \), the following is obtained:

\[
V(\mathbf{f}, t) = \frac{D}{4\pi \varepsilon_0} \int_0^{2\pi} \int_z^{z + \delta} f(z, \Theta, \psi) dz d\Theta
\]

\[
V(\mathbf{f}, t) = \frac{D}{4\pi \varepsilon_0} \int_0^{2\pi} \int_{z(t)}^{z(t) + \delta} \frac{\{R_{xy}(z_p - z) \cos \psi - \left[R_{xy}^2 - R_{xy}p_{xy} \cos(\Theta - \psi)\right] \sin \psi\} dz d\Theta}{\left[R_{xy}^2 + z^2 + \rho_{xy}^2 + z_p^2 - 2 \left[z_p + R_{xy}p_{xy} \cos(\Theta - \psi)\right]\right]^{1/2} \left[R_{xy}^2 + z^2\right]^{1/2}}
\]

### 2.2. Anatomical and Electrophysiological Parameter of the Colon

The values of the physical, anatomical and electrophysiological parameters of the ascending colon used to simulate the amplitude and the frequency of the slow waves are reported in Table 1 [8-15 35-36]. The length of the ascending colon and that of the greatest radius of haustra are the average values since those in the literature are not univocally defined.

**Table 1. Values of parameters used to simulate human colon slow waves.**

| Parameters                               | Values        |
|------------------------------------------|---------------|
| Dominant Frequency [8]                   | 4.57 cpm      |
| Highest Frequency [8]                    | 13.0 cpm      |
| Amplitude [8]                            | 0.1 - 0.5 mV  |
| Ascending colon length[33-34]            | 0.15 - 0.20 m |
| Haustrum radius                          | 0.04 - 0.07 m |
| Dipole moment \( \rho \) of annular band | 1.1 x 10-8 Coulomb x m |
| Annular band width \( \delta \)          | 0.00011 m     |
| Permittivity [30]                        | 2.65625 x 10^6 C^2/(N m^2) |

### 2.3. The Slow Wave Simulation

The slow waves as recorded with bipolar electrodes implanted in the muscular layer were simulated. The temporal variation in the electrical potential difference between two points on the surface of an ellipsoid, due to the periodic movement of the polarized annular band, was valued by performing a numerical Simpson integration in two dimension Eq. (4). To obtain slow waves plotted against time

The electrostatic potential \( V(\mathbf{\rho}) \) generated by an electric dipole of moment \( \mathbf{p} \) consisting of charges \( \pm q \) separated by a distance \( \lambda \) at a generic point \( P \) in the space at a distance \( \rho \) from the dipole for \( \rho > \lambda \) is:

\[
V(\mathbf{\rho}) = \left[1 / 4\pi \varepsilon_0 (\mathbf{\rho} \cdot \mathbf{\rho}) / \rho^3\right]
\]

Consequently, from Fig 1, if \( \mathbf{D} \) is the dipole density of the annular polarized band and \( \mathbf{p} \) is the dipole moment of the infinitesimal area \( dS \), being \( \mathbf{p} = \mathbf{D} dS \) then:

\[
V(\mathbf{f}) = \frac{1}{4\pi \varepsilon_0} \int_S \frac{\mathbf{p} \cdot \mathbf{R}}{\rho^3} dS
\]

Now expressing \( \mathbf{D}, \mathbf{\tau}, \mathbf{R} \) by means of the cartesian coordinates, after manipulation, the function to integrate becomes:

Since the annular band moves along the ellipsoids surface, z = z(t), then:

\[
V(\mathbf{f}, t) = \frac{D}{4\pi \varepsilon_0} \int_0^{2\pi} \int_{z(t)}^{z(t) + \delta} f(z, \Theta, \psi) dz d\Theta
\]

it was assumed that the band moved according to the law \( z(t) = v t \).

To simulate the slow waves the values of the length \( l_c = 0.20 \) m and of the radius \( r_h = 0.04 \) m (anatomical parameters), the values of the dipole moment \( \rho = 1.1 x 10^{-8} \) Coulomb x m of the annular band velocity \( v = 0.0157 \) m/s (physiological parameters) were taken as reference. Furthermore the inter-electrode distance of 0.005 m and the distance of 0.0235 m, from the lower edge of the second ellipsoid, to which the electrodes were positioned were taken as reference.

To examine the factors that modify the amplitude, the frequency and the phase of the slow waves and their observability, during the simulation process, we varied the dipole moment \( \rho \), the speed of the annular band \( v \), the length \( l_c \), and the largest radius \( r_h \) of the ellipsoids. Furthermore, the inter-electrode distance, and the electrode positioning with respect to the lower edge of the ellipsoids were varied.

The simulation program was written in the MATLAB language.

### 3. Results and Discussion

Illustrative examples of the colon slow waves as obtained by simulation are shown in Figures 2-6. The waveform in Figure 2a was obtained by keeping constant in every cycle of the annular band all the parameters used during the simulation process. The signal is periodic and the peak amplitude is constant.
The length $lc$ was taken as equal to 0.04 m. The inter-electrode distance was taken as equal to 0.005 m. The probe was placed at the distance 0.0235 from the lower edge of the second ellipsoid. The dipole moment was kept as constant and equal to $1.1 \times 10^{-8}$ Coulomb $\times$ m. The velocity of the annular band was 0.0157 m/s. The positive peak amplitude of the waveform is 0.5 mV. The measured period of the waveform is 12.76 s corresponding to the frequency 4.7 cpm.

The effect on the peak amplitude due to the modification of the dipole moment is shown in Figure 2b.

The amplitude of the peaks in Figure 2b is larger than that of the peaks in Figure 2a. Therefore the simulation pointed out that the increase in the dipole moment increases the amplitude of the slow wave peaks. The changes in the value of the dipole moment did not modify the slow wave frequency.

The effect due to the variation in the size of the radius $rh$ on the slow wave amplitude is shown in Figure 2c. The peaks’ amplitude is time-varying since $rh$ was varied in every cycle of the annular band. The simulation highlighted that the peaks’ amplitude decreased when $rh$ increased. The change of only 0.005 m in $rh$ was sufficient to modify the peak amplitude as can be seen by comparing the amplitudes of the first and of the second peak. The waveform is periodic since the length $lc$ of the colon tract was kept constant in every cycle of the annular band.

The effect on the slow wave waveform due to the modification of the inter-electrode distance is shown in Figure 3.

The simulation pointed out that the best inter-electrode distance was 0.0025 m. At a distance lower than 0.0025 m the...
positive peaks disappear and at a greater distance the waveform was greatly modified and the amplitude of the positive peaks decreased.

The simulation pointed out that also the electrode positioning with respect to the lower edge of the ellipsoids changed the amplitude of the positive and negative peaks. The best positioning was the distance 0.0235 m from the lower edge of each ellipsoid. For distances smaller or greater than 0.0235 m the amplitude decreased. We think that the results in Figure 2c and in Figure 3 may suggest a possible reason for the different values of the amplitude found comparing the results of the experiments made in vivo from several researchers and suggest that to make comparable the results obtained from different experiments it is important to standardize the electrode positioning and the inter-electrode distance.

The effect on the slow wave frequency due to the modification of the annular band velocity is shown in Figure 4. The period of the waveform in Figure 4 is larger than that in Figure 2a. The simulation pointed out that slow wave frequency decreased/increased when the annular band velocity was decreased/increased. This is a significant result because it indicates that, by increasing the annular band velocity, it is possible to simulate the burst activity.

The effects due to the modification of the length lc on the frequency and on the amplitude of slow wave are shown in Figure 5. Results highlighted that the decrease in lc made the frequency to increase. The amplitude of the waveform in Fig. 5 is lower than that of the waveform in Fig 2a since when lc was decreased rh was increased.

The effects due to the variation in the length lc on the phase lag, measured as delay time between the waveform recorded with one probe on the surface of the second ellipsoid and the waveform recorded with another probe placed on the surface of the third ellipsoid, are shown in...
Both probes were placed at a distance 0.0235 m from the lower edge of each ellipsoid. The inter-electrode distance was 0.005 m for both probes. The size of the radius \( r_h \) and of the length \( l_c \) were modified at the beginning of every cycle of the annular band. In Figure 6, a variable phase lag is observable between the waveform in solid line and the one in dotted line.

The waveforms in Figure 6 are not periodic since the time interval between contiguous peaks of the two waveforms varies from time to time. The variability of the amplitude, of the frequency and of the phase due to the modification of the length \( l_c \) may suggest a possible reason why the main features of the slow waves, as recorded with implanted bipolar electrodes, were highly irregular and time varying [10-17].

We think that the simulation results are significant since pointed out that the slow wave features (amplitude and frequency) can change not only by the modification of the physiological parameters but also by the geometrical modification of the haustra due to functional reasons and for recording conditions. In fact the simulations indicated that:

- the slow wave amplitude can be modified by varying only the dipole moment that physiologically is related to the number of cells that depolarize-polarize simultaneously in the annular band while maintaining constant the radius \( r_h \). Furthermore the amplitude can also be modified by changes in the radius \( r_h \) of ellipsoids, without making any change in the dipole moment;
- the frequency of the slow waves can be modified by varying only the speed of the annular band that physiologically is related to the velocity of the polarization-depolarization of cells while maintaining constant the length \( l_c \). Furthermore the frequency and the phase lag of slow waves can also be modified by changes in the length \( l_c \) of the colon segment without making any change in the annular band speed;
- the amplitude of the peaks of the slow waves was modified also by changes in the inter-electrode distance and in the positioning of the electrodes with respect to the lower edge of the ellipsoids.

The haustra of the colon were represented by ellipsoids since they are similar to them and since their equation may be easily implemented by computer. The analysis performed in this work considers the abdominal medium homogeneous as this assumption greatly simplifies the modeling.

4. Conclusion

Our results showed that the model offers the possibility to simulate the most significant characteristics of the electrical activity accurately enough, including some specific patterns such as frequency, phase and amplitude variations therefore the aims of the study were reached.

All the results obtained pointed out that the model is effective to explain the complexity of the colon electrical activity and may suggest possible reason concerning the discrepancy about the amplitude and the frequency reported from different researchers. Even if the recent tendencies are towards realistic but highly complex models, we think that the dipole model can be still useful since has the advantage of simplicity, allows to include the underlying physiology that is the basis of the motility mechanism and does not require large computing power as for some recent models but, it is feasible on a simple personal computer.

As future development we plan to utilize the model: a) to simulate the slow wave recordings made with electrodes placed on the abdominal surface and b) to analyzes the effects of the cutaneous electrode positioning and of the inter-electrode distance on the signal amplitude. Besides, we would verify the detectability with cutaneous electrodes of the frequency, amplitude and phase variations due to the changes of the sizes of ellipsoid axes.

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