Abstract

Introduction: Tissue oxygen saturation (StO2) and the vascular occlusion test (VOT) can identify tissue hypoperfusion in trauma and sepsis. However, the technique is neither standardized nor uses the same monitoring site. We hypothesized that baseline and VOT StO2 would be different in the forearm (F) and thenar eminence (TH) and that different minimal StO2 values during the VOT would result in different reoxygenation rates (ReO2).

Methods: StO2 and its change during the VOT were simultaneously measured in the F and TH, with 15 mm and 25 mm probes, using the 325 InSpectra monitor in 18 healthy, adult volunteers. Two VOTs were done to a threshold thenar StO2 of 40% interchanging the 15 mm and 25 mm probes between sites. Two additional VOTs were done to thresholds of 50% and 30%.

Results: BaseO2, DeO2, and ReO2 were different when measured in different anatomical sites (F and TH) and with different probe sizes, and ReO2 was different with differing VOT release StO2 threshold values. Thus, standardization of the site, probe and VOT challenge need to be stipulated when reporting data.

Introduction

Non-invasive measurements of tissue oxygen saturation (StO2) using near-infrared spectroscopy have been studied to assess tissue hypoperfusion in different populations. The absolute StO2 has been proven instrumental in predicting outcome in trauma patients [1,2]. These same studies, however, have shown limited discriminating capacity for the absolute StO2 value (sensitivity, 78%; specificity, 39%) and have even shown it to be at least as good as systolic blood pressure (sensitivity, 74%; specificity, 32%) [1]. The addition of a provocative test (ischaemic challenge) to the measurement of the StO2 would potentially enhance this discriminatory power between different cardiovascular states by creating emerging parameters to follow, such as the deoxygenation and reoxygenation slopes. Furthermore, the use of such provocative tests [3], specifically the vascular occlusion test (VOT), has been shown to improve and expand the predictive ability of StO2 to scenarios such as trauma, severe sepsis and septic shock [4,5].

The VOT is a provocative test in which StO2 is measured on a distal site (such as the thenar eminence (TH)) whilst a transient rapid vascular occlusion is performed, using a sphygmomanometer, for either a defined time interval (for

BaseO2 = baseline tissue oxygen saturation; DeO2 = deoxygenation rate; F = forearm; ReO2 = reoxygenation rate; StO2 = tissue oxygen saturation; TH = thenar eminence; VOT = vascular occlusion test.
example, 3 minutes) or until the StO₂ decreases to a defined minimal threshold. Once this threshold is reached, the vascular occlusion is released and the StO₂ is allowed to recover. Several emergent parameters arise from this technique, including the rate of deoxygenation (DeO₂), thought to reflect the local metabolic rate, the rate of reoxygenation (ReO₂), which reflects the time required to wash out stagnant blood and is thought to be determined by local cardiovascular reserve and microcirculatory flow, and the postobstructive hyperemic response.

The VOT, however, has not been standardized. In fact, multiple studies report results using different anatomical StO₂ measuring sites (TH, forearm (F), deltoid) [4,6-8], different near-infrared spectroscopy probe sizes (15 mm vs. 25 mm) [4,8-12], and different types and levels of deflation thresholds (StO₂ of 40%, 50%) versus time thresholds (3 minutes, 4 minutes, 5 minutes) [4,6,11,13]. Differences between anatomical sites may potentially affect near-infrared spectroscopy-derived parameters given the fact that fat and the muscle thickness distribution along the body is variable. Furthermore, given that increasing the sensing and illuminating probe distance augments the depth that near-infrared light travels, the use of different probes may screen different capillary beds at any given time. Finally, since the primary reason to perform the VOT is to produce a transient ischaemic challenge to note the subsequent ReO₂, the level of ischaemic challenge might vary for the same ischaemic time or threshold StO₂. As a consequence, caution must be taken when comparing results from the available literature on the VOT, as the test may be inadequate [14,15].

We hypothesized that absolute StO₂ values and VOT-derived StO₂ values obtained by monitoring different anatomical sites or using dissimilar depth may differ, and that different minimal StO₂ values during the VOT (deflation thresholds) would result in dissimilar ReO₂ rates.

Materials and methods
The present study was approved by the Institutional Review Board of the University of Pittsburgh. Informed consent was obtained from every volunteer enrolled in the study prior to performing any procedure.

Near-infrared spectroscopy
StO₂ and its change during the VOT were simultaneously measured in the F and TH, with 15 mm and 25 mm probes, using two 325 InSpectra® tissue spectrometers (Hutchinson Technology Inc., Minneapolis, MN, USA) on the same arm in 18 healthy, adult volunteers. Placement of the TH probe was done according to the manufacturer’s recommendations as previously described [4,9]. The F probe was placed over the Flexor digitorum profundus in the F.

Research software (InSpectra Version vBeta1.1; Hutchinson Technology Inc.) on two independent laptop computers was used for data collection.

Vascular occlusion test
The VOT was performed as previously described [9]. Briefly, the baseline arterial pressure was measured using a manual sphygmomanometer. An adult-size tourniquet cuff was then placed on the arm above both probes. After StO₂ signal stabilization at rest (<2% variation in 30 seconds), the tourniquet was inflated with an automatic pump (Portable Tourniquet System, ref. 9-2100-001; Delfi Medical Innovations Inc., Vancouver, BC, Canada) to >30 mmHg above systolic pressure and was kept inflated until the StO₂ decreased to 40% (deflation threshold). Inflation took approximately 3 to 4 seconds. The tourniquet was then rapidly deflated (<0.5 seconds) and the StO₂ response was followed until the StO₂ returned to baseline values. All repeated VOTs were performed after a minimal period of 5 minutes to allow the StO₂ to recover.

DeO₂ and ReO₂ slopes, the area under the curve of the hyperemic response as well as the duration of hyperemia (Figure 1) were calculated using the published methodology and a software package designed for this purpose and this specific tissue spectrometer (Version 3.03 InSpectra Analysis Program; Hutchinson Technology Inc.), as previously validated by us [9].

Protocol
Subjects were placed in a quiet environment while resting in a semirecumbent position with the studied arm resting over a cushion in the anatomical position. Probes were placed using a form-fitting plastic adhesive over the TH and volar surface.
of the F. The 15 mm probe was initially placed on the F and the 25 mm probe placed on the TH. A VOT was then performed. After a 5-minute resting period, the probe locations were switched (that is, the 15 mm probe to the TH, and the 25 mm probe to the F) and a second VOT was performed. Subsequently, two additional VOTs were carried out to StO2 deflation thresholds of 50% and 30% with the same probe disposition.

**Healthy volunteers**

Volunteers were selected according to the following inclusion and exclusion criteria: inclusion criterion, subjects older than 17 years (that is, ≥ 18 years); and exclusion criteria, acute or chronic cardiovascular or pulmonary disease, or subject taking any vasoactive medications.

**Statistical analysis**

Mean absolute StO2 values, the DeO2 and the ReO2 (%O2/minute) as measured by the 15 mm and 25 mm probes between the TH and F monitoring sites were compared using the Wilcoxon signed-ranks test. Comparison of the DeO2 and ReO2 when the VOT was performed at different StO2 deflation thresholds (that is, StO2 of 30%, 40% and 50%) was performed using the Friedman test and analysis of variance for repeated measures (after running normality tests). Results are presented as the median (interquartile range), P-value unless stated otherwise. Significance reports a difference between groups corresponding to \( P < 0.05 \) unless stated otherwise.

**Results**

Eighteen healthy volunteers were enrolled in the present study after obtaining informed consent. Demographic characteristics of the studied population are summarized in Table 1. The mean baseline StO2, DeO2, ReO2 and their coefficients of variability for these measures for the various comparisons are summarized in Table 2.

The absolute StO2, DeO2 and ReO2 values for a deflation threshold of 40% were different between the TH and F for both the 15 mm and 25 mm probes (Figures 2 and 3), and were also different at the TH site for the 15 mm and 25 mm probes (Figure 4). Not surprisingly, the TH DeO2 was not altered by varying the deflation StO2 thresholds from 30% to 50% when measured with the 15 mm probe. This result was expected given that the DeO2 is dependent on the metabolic conditions of the tissue, independent of the intensity of the ischemic insult and given the specific calculation methodology [1]. If the metabolic rate of the sampled tissue was not varied, therefore, the DeO2 should not be significantly modified. The ReO2 was higher using the 30% threshold than either the 40% or 50% thresholds, which themselves were similar (Figure 5).

The coefficients of variability for the absolute StO2, DeO2 and ReO2 values were also different when comparing both sites and probes, being less with the TH than F measures and with the 15 mm than 25 mm probe size. We also observed a lower coefficient of variability with 40% and 50% thresholds as compared with the 30% threshold (Table 3).

**Discussion**

Baseline StO2 values and their emergent parameters of the DeO2 and the ReO2, assessed by the VOT, are dependent on the site of measurement, the probe size and, to a certain extent, the ischemic challenge. Varying any one of these components will significantly vary StO2-related measures independent of the baseline cardiovascular status. When making inferences about cardiovascular function using these measures, therefore, care must be taken in comparing or

| Characteristic | Value |
|---------------|-------|
| Age (years)   | 32.9 ± 8.2 |
| Gender        |       |
|   Female      | 6 (33%) |
|   Male        | 12 (67%) |
| Race          |       |
|   Caucasian   | 10 (56%) |
|   Hispanic    | 4 (22%) |
|   Asian       | 3 (17%) |
|   Indian      | 1 (5%) |
| Weight (kg)   | 75.5 ± 15.5 |
| Height (cm)   | 175.8 ± 8.2 |
| Temperature (°C) | 36.1 ± 0.6 |
| Systolic blood pressure (mmHg) | 118 ± 12 |
| Diastolic blood pressure (mmHg) | 73 ± 7 |
| Mean arterial pressure (mmHg) | 88 ± 8 |
| Heart rate (beats/minute) | 69 ± 9 |

Data are presented as mean ± standard deviation or n (%).
combining results from different studies that use different measurement techniques and protocols. Presently, the VOT ischaemic challenge has not been standardized. Several investigators report the DeO₂ and the ReO₂ from a fixed ischaemic time (for example, 3 minutes) rather than to a defined threshold StO₂ value. Since the basal metabolic rate can vary amongst subjects, varying the DeO₂ proportionally using a fixed ischaemic time will result in differing threshold StO₂ values within and among subjects, making changes in the ReO₂ difficult to interpret among subjects if their metabolic rates are also different because they will reach different StO₂ nadirs for a constant ischaemic time. Our data therefore support using a defined ischaemic StO₂ threshold in future studies to minimize ReO₂ variability.

### Table 2

Baseline tissue oxygen saturation, deoxygenation and reoxygenation rates between sites and between probe sizes

| Probe | Thenar eminence | Coefficient of variability (%) | Forearm | Coefficient of variability (%) | \( P \) value\(^a\) |
|-------|-----------------|-------------------------------|---------|-------------------------------|-----------------|
| 15 mm | Absolute StO₂ (%) | 90.4 (85.2, 93.5), 76.6 to 95.3\(^b\) | 5.6 | 85.2 (80.7, 90.2), 65.8 to 93.6\(^b\) | 7.8 | 0.031 |
|       | DeO₂ (%O₂/minute) | \(-12.8 (-16.2, -11.3)\) | 26.1 | \(-8.5 (-10.3, -7.8)\) | 42.7 | 0.011 |
|       | ReO₂ (%O₂/minute) | 297.2 (213.7, 328.6) | 21.5 | 98.6 (53.7, 157.8) | 68.4 | <0.0001 |
| 25 mm | Absolute StO₂ (%) | 92.7 (89.4, 94.7), 81.9 to 95.9\(^b\) | 4.6 | 87.3 (81.7, 90.9), 76.0 to 95.2\(^b\) | 6.7 | 0.016 |
|       | DeO₂ (%O₂/minute) | \(-18.0 (-24.1, -14.8)\) | 36.5 | \(-9.9 (-15.3, -6.5)\) | 53.6 | <0.0001 |
|       | ReO₂ (%O₂/minute) | 401.6 (331.7, 543.2) | 28.2 | 160.5 (132.3, 366.9) | 66.8 | 0.012 |

Comparison of 15 mm vs. 25 mm probe \( (P \) value)\)

- StO₂: 0.020
- DeO₂: <0.0001
- ReO₂: <0.0001

Baseline tissue oxygen saturation (StO₂), deoxygenation rate (DeO₂) and reoxygenation rate (ReO₂) between the thenar eminence versus forearm and between the 15 mm probe versus 25 mm probe. Data presented as the median (interquartile range). \(^a\)Thenar eminence versus forearm comparison. \(^b\)Absolute StO₂ range.

**Figure 2**

TH\(_{15\text{mm}}\) vs. F\(_{15\text{mm}}\)

Box plots comparing tissue oxygen saturation (StO₂) parameters measured with the 15 mm probe at different anatomical sites. DeO₂, deoxygenation rate; ReO₂, reoxygenation rate.
We found that the baseline StO₂, DeO₂ and ReO₂ values were consistently higher in the TH than F sites. Furthermore, the magnitude of the difference between the TH and F was greater for DeO₂ and ReO₂ values than for baseline StO₂ values. There was also a trend toward a greater variability for baseline StO₂ at F than at TH sites. This variability was increased for the DeO₂ and ReO₂. Although our study does not allow us to identify why this difference occurs, most probably it reflects the greater degree of tissue and the associated vascular variability present in the F over the TH. The F has a variable layer of subcutaneous fat, which has a lower metabolic rate and minimal microcirculatory density when compared with muscle. The TH has almost no fat and is highly consistent amongst subjects. Our data therefore support using the TH site rather than the F site when measuring StO₂ and its VOT-related parameters.
We also found consistently lower baseline StO\textsubscript{2} values with the 15 mm probe than with the 25 mm probe, and this difference increased with VOT-related parameters. Although baseline StO\textsubscript{2} values displayed a similar variability (5.6\% vs. 4.6\%), VOT-derived measurements performed with the 15 mm probe showed less variability than those performed with the 25 mm probe. Presumably, by sampling a smaller amount of tissue volume, the 15 mm probe is less subject to measurement error. Our data support the routine use of the 15 mm probe over the 25 mm probe in future studies.

The hyperemic response, as quantified by the area under the curve and the duration, varied according to the anatomical site of measurement and the probe size used. Furthermore, great variability was found among healthy volunteers with regards to both parameters, as previously pointed out by our group [9]. These results suggest that the hyperemic response is not a reproducible parameter, and has been proven to be highly dependent on individual variability. Thus, it may not be a reliable parameter for clinical use.

**Limitations**

The present study has two primary limitations.

First, we studied only two anatomical sites, whereas StO\textsubscript{2} can be measured anywhere on the body. Extrapolation of these findings to other anatomical sites, such as the abdominal wall, thigh and masseter muscles, should be done with caution.

Second, we did not study critically ill patients but healthy volunteers. Although this was the goal of the study, its application to critically ill patients might be limited. Previous
studies by ourselves and others document that cardio-
vascular insufficiency can markedly increase intersubject
variability [4,9]. Our data demonstrated a consistently lower
coefficient of variation whenever the combination of TH site
and 15 mm probe was used, which suggests that this site
may also yield more consistent data in clinical trials. Similarly,
using a defined ischaemic threshold for the VOT, method-
specific variability of the ReO₂ should also be minimized.

Competing interests
HG, JM and HKK are co-investigators in a Hutchinson-
sponsored clinical trial. CI has received honorarium for
speaking at a Hutchinson Symposium, and is a co-
investigator on a Hutchinson-sponsored clinical trial. MRP
and JCP have received an honorarium for speaking at a
Hutchinson Symposium, and are co-investigators on a
Hutchinson-sponsored prospective clinical trial. PS declares
that he has no competing interests.

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Box plot comparison of the hyperemic response between anatomical sites and probe sizes. AUC, hyperemic area under the curve.