Efficiencies of Some Spherical Ion Chambers in Continuous and Pulsed Radiation: A Numerical Evaluation

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Summary

Background: Evaluation of the collection efficiencies of ion chambers is a necessity for the proper evaluation of radiation quantities in different applications. Overall collection efficiency is the product of three different values: collection efficiencies considering contributions of, volume recombination, back-diffusion loss and initial recombination, the later may be neglected at low charge rates.

Material/Methods: Five common spherical ion chambers of different volumes and specifications were included in this study for the evaluation of volume recombination collection efficiency and back diffusion collection efficiency for continuous and pulsed radiation and at different values of the applied polarizing potential. Through current work there is an attempt of focusing on how the selection of ion chamber dimensions may affect the overall collection efficiency in addition to the proper selection of other influencing parameters.

Results: Collection efficiencies considering volume recombination ($f_v$) for five spherical ion chambers of common types were evaluated for continuous and pulsed radiation over a wide range of polarizing potential. The relation between the ion chamber volume and its evaluated collection efficiencies were studied for both continuous and pulsed radiation; transit time values for the ion chambers included in this study were evaluated at different values of applied potential. Also, collection efficiencies considering diffusion current values ($f_d$) were evaluated for the five chambers, and plotted versus the applied polarizing potential.

Conclusions: Through this study it was feasible to evaluate numerically the collection efficiencies of some spherical ion chambers considering volume recombination and back diffusion effects; the affecting parameters were studied and highlighted.

MeSH Keywords: Air Ionization • Efficiency • V(D)J Recombination

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The importance of ion chamber efficiency evaluation as a basic step in the determination of radiation doses in medical radiation applications is reflected by the accuracy requirements recommended for the delivery of tumor dose as the final step where it was recommended that ±5% should be the maximum uncertainty associated to this process [1]. This value of maximum uncertainty associated to the delivery of tumor dose includes all factors associated or related to this process such as uncertainty in basic dosimetry, patient positioning, and errors in clinical settings [2].

In basic dosimetry, the aim is to evaluate experimentally some radiation quantity according to well-recognized procedures and using associated formulations and recommended equipment and tools. This is usually achieved via dosimetry protocols [3–7]. The most common dosimetry
systems used worldwide in basic dosimetry for all medical applications are the ion chambers [8].

When incident radiation interacts with the ion chamber walls, build-up cap, sleeve, or phantom through photoelectric effect, Compton scattering and pair production (according to conditions of interactions, it usually results in the production of energetic electrons; when these electrons enter the sensitive volume of the ion chamber, they ionize air inside the sensitive volume of the chamber which results in the production of positive ions and low energy electrons. The later can be attached easily by oxygen molecules forming negative ions [2].

Ideally, all charges produced within the volume of the ion chamber are collected by the corresponding electrode. However, some factors lead to the lack of complete collection of these charges [9]. These factors are related to different origins either connected with the geometrical structure of the ion chamber, applied voltage, or the beam type and strength [10,11].

Cavity ion chambers are of two types, either parallel-plate ion chambers usually used for the superficial x-rays, low energy electrons, and for surface doses evaluation, or the thimble type chambers usually used in photon or electron beams above 10 MeV.

In the current work, collection efficiencies of some spherical ion chambers are evaluated numerically in order to find out differences among types or models in general, although it still necessary to evaluate experimentally some related correction factors for each individual ion chamber within the same type. It is important to note that this work is just an academic study and hence it was not restricted to those values of the applied potential recommended by the manufacturer in calculations. The dimensional characteristics of spherical chambers included in the current study are included in Table 1, and air was assumed to be the filling gas.

Material and Methods

Away from the ideal saturation current in an ionization chamber (I*), real output current (I) is usually lower due to incomplete charge collection as a result of several effects, being: Initial recombination, Back-diffusion to electrodes, and Volume recombination [12]. The collection efficiency for an ion chamber (f) can be evaluated according to the following relation:

\[ f = f_i f_v f_d \]  \[(1)\]

where \( f_i \), \( f_v \), and \( f_d \) are collection efficiencies considering contributions of initial recombination, volume recombination, and back-diffusion loss, respectively [13]. Initial recombination (also called columnar recombination) does not depend on the radiation dose or dose rate. This process occurs when the positive and negative ions formed in the same charged-particle track meet and recombine. For initial recombination, the number of tracks formed within the chamber is not important and hence this effect is dose-rate independent. In contrast, volume recombination (also called general recombination) takes into account recombination of ions formed from different origins (different tracks) and hence the number of tracks formed within the chamber affects the value of the general recombination and hence it is dependent on the radiation dose rate [14,15], the total recombination is the sum of these two effects. Additionally, loss of ions due to diffusion is independent on the radiation dose rate and considers the back diffusion of positive and negative ions to an anode and cathode respectively [16].

Initial recombination is most probable in high ion density tracks like those formed by alpha particles or other high LET radiation, like energetic electrons passing through high-pressure gases while it is negligible in usual clinical uses and other cases.

So, for the recombination process we will consider only volume recombination in the current study. For continuous radiation, and according to the Bohr’s theory [17], the collection efficiency \( f_v \) can be obtained from the following formula:

\[ f_v = 1 - \eta^2 \]  \[(1)\]

where \( \eta^2 = \left(\frac{M^2}{6}\right) \frac{d^2 \dot{q}}{V^2} \)  \[(2)\]

and \( d \) is an effective electrode spacing, \( M \) is an empirical constant depending on the nature of the gas (1.99 x 10^{-2} ± 1.7% Vm^{-1/2} C^{-1/2} for air), \( \dot{q} \) is the rate of charge collected per unit volume of the gas (cm^{-3}s^{-1}), and \( V \) is the polarizing potential [18].

In case of pulsed radiation, \( f_v \) can be calculated using the following formula:

\[ f_v = \frac{\nu}{\exp(\nu) - 1} \]  \[(3)\]
Figure 1. Evaluated collection efficiencies in continuous radiation for different ion chambers as a function in the applied polarizing potential in an ascending order with respect to the chamber volume, values evaluated at different values of charge rate per unit volume ($q$):

(A) A3-Exradin, (B) A4-Exradin, (C) A5-Exradin, (D) A6-Exradin, (E) A8-Exradin.
And hence the collection efficiency corresponding to back diffusion, \( K \) is the Boltzmann constant, \( T \) is the air temperature, \( q \) is the initial charge density per pulse of the positive and negative ions collected by the ion chamber during irradiation, \( \alpha \) is the ion recombination coefficient, \( e \) is the charge of an electron, \( k_1 \) is the mobility of positive ions, \( k_2 \) is the mobility of the negative ions, and \( \mu \) depends on the lifetime of ions in the chamber and for air it equals to 3.02 \( \times 10^{-3} \) cm\(^{-3}\)s\(^{-1}\) [19].

The effective electrode spacing for the spherical chambers \((d)\) can be calculated using the following formula [17–20]:

\[
d = \frac{(a-b)}{\sqrt{3}} \left( \frac{a}{b} + 1 + \frac{b}{a} \right) \tag{6}
\]

Where ‘a’ is the internal radius of the outer electrode and ‘b’ is the external radius of the inner electrode.

For the decrease in output current due to back diffusion in spherical chambers, an approximate solution was presented by Takata, N. et al. [21]:

\[
\frac{\delta I}{I_s} = 1 - \frac{ab}{b + (a-b)(KT/eV)} - \frac{ab}{a - (a-b)(KT/eV)} \tag{7}
\]

Where \( \delta I \) is the fraction of current loss due to back diffusion, \( K \) is the Boltzmann constant, \( T \) is the air temperature, \( e \) is the elementary charge, and \( V \) is the applied polarizing potential.

And hence the collection efficiency corresponding to back diffusion loss \((f_d)\) can be expressed as follows:

\[
f_d = 1 - \frac{\delta I}{I_s} \tag{8}
\]
Figure 3. Evaluated collection efficiencies ($f_V$) in pulsed radiation for different ion chambers as a function in the applied polarizing potential in an ascending order with respect to the chamber volume, values evaluated at different values of charge rate per unit volume ($\dot{q}$): (A) A3-Exradin, (B) A4-Exradin, (C) A5-Exradin, (D) A6-Exradin, (E) A8-Exradin.
decrease of \( f_v \) as the chamber volume increases, this may be due to the special geometrical or technical requirements for the design of large-volume ion chambers. Similar figures like Figure 2 can be plotted for other \( V \) values.

**Pulsed radiation**

Volume collection efficiencies \( f_v \) were evaluated for the five ion chambers under study for pulsed radiation and plotted as shown in Figure 3 which represents saturation curves for the A3 Exradin ion chamber (Figure 3A), A4 (Figure 3B), A5 (Figure 3C), A6 (Figure 3D), and A8 (Figure 3E) over a wide range of polarizing potential (150–1200 V), which is not limited to values recommended by the manufacturer.

As shown in Figure 3A, a wide range of charge density per pulse \( q \) values were used for the evaluation of \( f_v \) where \( q \) ranged from \( 1.0 \times 10^{-4} \) to \( 4.23 \times 10^{-3} \) cm\(^{-3}\)/pulse. The same range for \( q \) values was used in Figure 3B–3D, while for Figure 3E a range from \( 13 \times 10^{-6} \) to \( 1.0 \times 10^{-4} \) cm\(^{-3}\)/pulse was used for the evaluation of \( f_v \). Similar to the case of continuous radiation, curves corresponding to high ionization charge density per pulse \( q \) do not reach saturation even at a very high applied polarizing potential \( V \); this encounters a significant ion recombination.

Figure 4 represents the relation between the chamber volume (cm\(^3\)) and the evaluated collection efficiencies \( f_v \) over a wide range of charge density per pulse \( q \) values at...
polarizing potential of $V = 700$ V. From Figure 4, and despite the absence of a certain behavior regarding the change in $v_f$ as a function in the chamber volume, it is noticeable that $v_f$ decreases as the chamber volume increases; for example at the same charge density per pulse, $q = 7.8 \times 10^{-4} \text{ cm}^3/\text{pulse}$ which is corresponding to a high ionization intensity, $v_f$ for the A4 ion chamber is found to be 1.27%, i.e. less than that for the A3 ion chamber and 1.89% higher than that for the A5 ion chamber, while the A6 ion chamber had $v_f$ of about 12.27%, i.e. less than A5 and a very poor value for the A8 ion chamber because of the high q value. At a much lower q value, $q = 1.3 \times 10^{-5} \text{ cm}^3/\text{pulse}$, $v_f$ values became better and closer to each other; $v_f$ for the A4 ion chamber was only 0.02% lower than that for A3, and 0.03% higher than $v_f$ of the A5 ion chamber, while A6 showed $v_f$ value of 0.21% lower than that of A5 and even the A8 ion chamber volume efficiency, $v_f$ was 0.9971 which was 2.88% lower than that of A3.

For large chambers, it was found that recombination effects due to transit-time effects is quite significant [23]. This may be the reason for lower $v_f$ values for larger chambers compared to the small ones. Transit time ($\tau_i$) for ions in an ionization chamber can be estimated according to the following formula [23]:

$$
\tau_i = \frac{d^2}{V k_f} \quad (9)
$$

where $V$ is the applied potential, $d$ is the effective electrode separation, and $k_f$ is the mobility of the produced ion and was assumed to be $1.58 \times 10^{-4} \text{ m}^2\text{V}^{-1}\text{s}^{-1}$ [24]. Transit time ($\tau_i$) was evaluated for the chambers included in this study and over a range of the applied potential of $(200-1200)$ V and is represented in Figure 5. As shown in that figure, transit time decreased in a power trend as the applied potential (V) increased, and it is clear from the inset of the figure that at constant V, transit time increases as the chamber volume increases. For the chamber A3, $\tau_i$ was 0.078 s at 200 V of the applied voltage, and reached 0.0013 s at 1200 V. On the other hand, A6, the largest among the studied ion chambers, had a $\tau_i$ value of 1.097 s at 600 V while it decreased to become 0.548 s at $V = 1200$ V. Close values were obtained by Geilejns et al., [23] where transit time ($\tau_i$) was evaluated for the A5 Exradin ion chamber resulting in a value of 0.050 s at an ambient polarizing potential (300 V). The value obtained through this work for the same conditions was 0.045 s. However, dimensions mentioned for the A5 ion chamber are slightly different from those mentioned in this work.

**Back diffusion**

The collection efficiency corresponding to back diffusion loss ($f_d$) for different ion chambers was evaluated according to the equation (8). As shown in Figure 6, $f_d$ increased non-linearly as the applied polarizing potential increased; according to the figure, the highest value of $f_d$ was achieved by two ion chambers, A5 followed by A3 and A4, while the lowest values of $f_d$ were those of A6 and A8, for example, at a value of the applied polarizing potential $V = 500$ V, $f_d$ was 99.88% for A5, and 99.87% for A3 and A4, while for A6 and A8 it was 99.86% and 99.80%, respectively.

Figure 7 represents the relation between the ratio of the inner radius of the outer electrode to the outer radius of the inner electrode (a/b) and the calculated values of $f_d$. This relation is an inversely linear relation, as it clearly follows from the figure, i.e. as the ratio a/b increases, the values of $f_d$ decrease. The range of (a/b) values was started by 8.8 which corresponded to A5 Exradin, followed by 9.10 for A3, 9.29 for A4, 9.86 for A6 and it ended at the value of 13.89 for A8. A linear relationship was confirmed for different values of the applied polarizing potential ranging from 150 V to 1000 V.

**Conclusions**

Collection efficiencies considering volume recombination were evaluated for five spherical ion chambers of common types and of different volumes ranging from 3.6 cm$^3$ to 15700 cm$^3$, for continuous and pulsed radiation over wide ranges of polarizing potential. The relation between the ion chamber volume and its evaluated collection efficiencies were studied for both continuous and pulsed radiation; transit time for the ion chambers included in this study was evaluated at different values of applied potential. Also, diffusion current values were evaluated for those chambers and hence their collection efficiencies considering diffusion current were calculated and plotted versus the applied polarizing potential and versus the (a/b) ratio. It was found that $f_d$ increases as the applied polarizing potential increases non-linearly and decreases linearly as the (a/b) ratio increases.

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