Biocompatibility and biosafety of butterfly wings for the clinical use of tissue-engineered nerve grafts

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Abstract
In a previous study, we used natural butterfly wings as a cell growth matrix for tissue engineering materials and found that the surface of different butterfly wings had different ultramicrostructures, which can affect the qualitative growth of cells and regulate cell growth, metabolism, and gene expression. However, the biocompatibility and biosafety of butterfly wings must be studied. In this study, we found that Sprague-Dawley rat dorsal root ganglion neurons could grow along the structural stripes of butterfly wings, and Schwann cells could normally attach to and proliferate on different species of butterfly wings. The biocompatibility and biosafety of butterfly wings were further examined through subcutaneous implantation in Sprague-Dawley rats, intraperitoneal injection in Institute of Cancer Research mice, intradermal injection in rabbits, and external application to guinea pigs. Our results showed that butterfly wings did not induce toxicity, and all examined animals exhibited normal behaviors and no symptoms, such as erythema or edema. These findings suggested that butterfly wings possess excellent biocompatibility and biosafety and can be used as a type of tissue engineering material. This study was approved by the Experimental Animal Ethics Committee of Jiangsu Province of China (approval No. 20190303-18) on March 3, 2019.

Key Words: biocompatibility; biomaterials; biosafety; butterfly wings; dorsal root ganglion; neurons; Schwann cells; tissue engineering

Introduction
Materials are key elements of tissue engineering and cell-based therapies (Guthrie et al., 2013; Facklam et al., 2020; Vermeulen and de Boer, 2020). Various materials, including bioinert and bioactive materials, have been applied clinically to repair diverse tissues and organs (Yi et al., 2019). Synthetic non-degradable materials, such as silicone and polyethylene glycol, and synthetic degradable materials, such as polyglycolic acid, polyactic acid, and poly (lactin-co-glycolic acid), have been widely applied in the fields of tissue engineering and regenerative medicine (Yu et al., 2017; Qian et al., 2019). Recently, naturally derived materials have begun to attract attention (Ghosh et al., 2019). Naturally derived materials present many advantages, such as abundant resources, excellent biological performance, and similar mechanical properties to tissues and organs, and thus have been developed for many clinical applications.

Chitosan, a natural, polycationic, linear polysaccharide that is derived from chitin, has commonly been used in the construction of neural scaffolds and the treatment of peripheral nerve injury (Wang et al., 2005; Stenberg et al., 2016; Bhatt et al., 2017; Crosio et al., 2019; Dietzmeyer et al., 2020; Yu et al., 2020). Butterfly wings are natural biomaterials composed of chitin (Elbaz et al., 2017), which possess fine micro-/nano-surface structures and have been utilized as a biomimetic material (Mu et al., 2013; Zhang et al., 2015). In our previous study, butterfly wings were collected from Morpho menelaus (M.m.) and Papilio ulysses telegonus (P.u.t.), two types of butterflies with divergent wing-surface topographies, to observe the influence of wing structures and surface features on Schwann cell arrangements. Our results indicated that Schwann cells cultured on M.m. wings,

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the surfaces of which are composed of grooves, exhibited a regular sorting pattern, whereas Schwann cells cultured on *P. u. t.* wings, the surfaces of which are composed of micro-/nano-concaves, exhibited randomized growth (He et al., 2018). These outcomes suggested that *M. m.* wings may be suitable for Schwann cell growth and peripheral nerve repair (He et al., 2018).

For the successful regeneration and functional recovery of injured peripheral nerves, implanted biomaterials should have good biocompatibility not only with Schwann cells but also with neuronal axons. Therefore, in the current study, dorsal root ganglion (DRG) neurons were collected and cultured on *M. m.* wings to determine the biocompatibility of *M. m.* wings with DRG neurons. The proliferation and attachment of Schwann cells on butterfly wings were also evaluated. Moreover, butterfly wings or butterfly wing extracts were applied to various types of animals, including Sprague-Dawley rats, Institute of Cancer Research (ICR) mice, rabbits, and guinea pigs, to examine the biosafety of these materials. The biocompatibility and biosafety evaluation of butterfly wings would increase the clinical applications of natural materials that present with biomimetic structures.

**Materials and Methods**

**Animals**

Embryonic day 14 (E14), specific-pathogen-free, Sprague-Dawley rats were used to obtain DRG cultures. Postnatal, 1–2-day-old, specific-pathogen-free, wild-type, Sprague-Dawley rats (*n* = 20) and green fluorescent protein-transgenic Sprague-Dawley rats (*n* = 20) were used to obtain Schwann cell cultures. A total of 36 adult male Sprague-Dawley rats (specific-pathogen-free level weighing 200–250 g), 28 adult ICR mice (specific-pathogen-free level, half female and half male, weighing 18–20 g), nine adult white rabbits (6-month-old, clean level, weighing 2.5–3 kg), and 32 healthy adult guinea pigs (clean level, 1.5-year-old, weighing 350–400 g) were obtained from the Experimental Animal Center of Nantong University, China (license Nos. SYXK [Su] 2017-0045 and SYXK [Su] 2017-0046).

All procedures were conducted in accordance with the Institutional Animal Care guidelines of Nantong University and were approved by the Experimental Animal Ethics Committee of Jiangsu Province, China (approval No. 20190303-18) on March 3, 2019.

**Butterfly wing fabrication**

*M. m.* and *P. u. t.* wings, purchased from Beijing Yuxiao Media (Beijing, China), were prepared as described previously (He et al., 2018). Briefly, butterfly wings were exposed to 1 M HCl for 15 minutes. The wings were then sterilized by overnight immersion in 70% ethanol and ultraviolet radiation properties. Treated butterfly wings were then sterilized by 2 hours and 2 M NaOH overnight to increase their hydrophilic properties. Chitosan, a widely used biomaterial in tissue engineering with no detectable side effects, was used as a control. Chitosan (Nantong Water Products Institute, Nantong, China) with a deacetylation degree of 92.5% and a viscosity of 0.11 Pa·s was dissolved in 2% acetic acid, added to a culture dish, and frozen into a film. Frozen chitosan films were neutralized with 5% NaOH for 30 minutes, washed with distilled water, soaked overnight in Dulbecco’s modified Eagle’s medium containing 10% fetal bovine serum (Gibco, Grand Island, NY, USA) and 1% penicillin and streptomycin for 24 hours. Cytosine arabinoside (10 µM, Sigma, St Louis, MO, USA) was added to the cell culture medium for 24 hours, and then 2 µM forskolin (Sigma) and 50 ng/mL heregulin (Sigma) were supplied to the culture media. Cells were then purified by the addition of anti-Thy1.1 antibody (1:1000; Sigma) and rabbit complement protein (1:3; Sigma) to remove contaminating fibroblasts.

**Immunofluorescence staining**

DRG explants cultured on the wings of *M. m.* and *P. u. t.* were fixed in 4% paraformaldehyde overnight at 4°C, and incubated in 0.5% Triton X-100 (Sigma) in phosphate-buffered saline, blocked in 5% bovine serum albumin (Thermo Scientific, Rockford, IL, USA) for 1 hour, and incubated in primary antibody, overnight at 4°C. Primary antibody incubations were performed with the following specifications: anti-S100 (a Schwann cell marker; mouse; 1:100; Cat# ab14849; Abcam, Cambridge, MA, USA) and anti-β-tubulin III (a neuron marker; rabbit; 1:100; Cat# ab18207; Abcam). Secondary antibody incubations were performed using goat anti-mouse IgG (Alexa Fluor594, 1:300; Cat# ab150120; Abcam), donkey anti-rabbit IgG (Alexa Fluor488, 1:300; Cat# ab150073; Abcam) at 37°C for 2 hours, followed by counterstaining with Hoechst 33342 (1 µg/mL; Sigma). Images were taken using a Zeiss fluorescence confocal microscope (Leica, Wetzlar, Germany).

**Scanning electron microscopy**

DRG explants and cells cultured on *M. m.* wings were fixed in 4% paraformaldehyde overnight at 4°C, post-fixed with 1% OsO4, gradually dehydrated in acetone, and dried in a critical point drier (Hitachi, Tokyo, Japan). Samples were coated with gold in a JFC-1100 unit (JEOL Inc., Tokyo, Japan) for subsequent observations. Images were taken using a scanning electron microscope (S-3400N; Hitachi).

**Proliferation and adhesion assays**

The proliferation rate of Schwann cells was determined using the Cell-Light™ EDU DNA Cell Proliferation Kit (Ribobio, Guangzhou, China). Schwann cells, treated with 50 µM 5-ethynyl-2′-deoxyuridine (EdU) for 24 hours at 37°C, were fixed in 4% paraformaldehyde for 30 minutes and stained with Hoechst 33342 (1 µg/mL; Sigma). Schwann cell adhesion to the wings was detected after 6 hours of culture using 3,3′-diododecylxylcarbocyanine perchlorate (DiO, Invitrogen) fluorescent dye. Images were taken using a Zeiss fluorescence microscope (Axio Imager M2; Jen, Germany).

**In vivo experiments**

*M. m.* wings and chitosan film were cut into 1 cm × 1 cm pieces and subcutaneously implanted into the backs of rats, and the blood cellular parameters were assessed using poly-L-lysine hydrobromide for subsequent studies.

**DRG culture**

DRGs were dissected from embryonic day (E) 14 rats, as previously described (Liu et al., 2019). Isolated DRGs were digested with 0.5 mg/mL collagenase (Roche, Basel, Switzerland) for 2 hours and 0.125% trypsin (Thermo Fisher Scientific, Waltham, MA, USA) for 30 minutes at 37°C. DRG explants (3–4 DRG explants/cm2) and isolated DRG cells (103–104/L) were seeded onto butterfly wings and cultured for 24 hours at 37°C.

**Schwann cell culture**

Schwann cells were harvested as previously described (Liu et al., 2019). Briefly, sciatic nerves were isolated from postnatal wild-type rats and green fluorescent protein-transgenic rats and digested with 3 mg/mL collagenase for 30 minutes and 0.125% trypsin for 10 minutes at 37°C. Isolated Schwann cells were cultured in Dulbecco’s modified Eagle’s medium containing 10% fetal bovine serum (Gibco, Grand Island, NY, USA) and 1% penicillin and streptomycin for 24 hours. Cytosine arabinoside (10 µM, Sigma, St Louis, MO, USA) was added to the cell culture medium for 24 hours, and then 2 µM forskolin (Sigma) and 50 ng/mL heregulin (Sigma) were supplied to the culture media. Cells were then purified by the addition of anti-Thy1.1 antibody (1:1000; Sigma) and rabbit complement protein (1:3; Sigma) to remove contaminating fibroblasts.
Peripheral blood samples were collected from the rats 4 weeks after implantation. Various blood cellular parameters, including alanine aminotransferase, aspartate aminotransferase, blood urea nitrogen, creatinine, uric acid, lactate dehydrogenase, alkaline phosphatase, and creatine phosphokinase, white blood cells, neutrophil percentages, and lymphocyte percentages, were measured: the values for alanine aminotransferase, aspartate aminotransferase, blood urea nitrogen, creatinine, uric acid reflected renal function; creatine andurine acid reflected kidney function; lactate dehydrogenase indicated cellular status and cell toxicity; and the numbers of white blood cells and the percentages of neutrophils and lymphocytes indicated immune status (Liu et al., 2016; Park et al., 2016). After acid and alkali treatment, M.m. wings were immersed in normal saline using various ratios of surface areas to saline volumes to obtain 3, 6, and 12 cm²/mL M.m. wing extracts. Various concentrations of M.m. wing extracts were injected into animals to perform the following tests: intraperitoneal injections into ICR mice were used to perform a systemic acute toxicity test; intradermal injections into the backs of rabbits were used to perform intradermal injection reaction tests; and external applications were used on guinea pigs to perform skin sensitization tests, as previously described (Sun et al., 2019; Sun et al., 2020). A total of 28 specific-pathogen-free ICR mice were randomly divided into four groups (wing male, wing female, normal saline male, and normal saline female groups), containing seven mice in each group. The intraperitoneal cavities of the ICR mice were injected with 6 cm²/mL M.m. wing extract (50 mL/kg) or normal saline (50 mL/kg). Mice were observed and weighed at 24, 48, and 72 hours after injection. Nine adult white rabbits were randomly divided into three groups (3, 6, and 12 cm²/mL M.m. wing extracts), containing three rabbits per group. The left back area of each rabbit was intradermally injected with M.m. wing extracts at five points (0.2 mL/point) on the left side of the spine, whereas the right back area was injected with normal saline at five points (0.2 mL/point) on the right side of the spine. The reactions observed in the local and surrounding skin, such as erythema, edema, and necrosis, were observed at 24, 48, and 72 hours after injection. M.m. wing extracts were externally applied to the left abdomens of guinea pigs to perform the skin sensitization test. In total, 32 adult guinea pigs were randomly divided into four groups (12 cm²/mL M.m. wing extract, 6 cm²/mL M.m. wing extract, 4% formaldehyde, and normal saline) containing eight guinea pigs per group. As a positive control, 4% formaldehyde was applied, whereas saline was applied as the negative control. Animal skin reactions at each point were evaluated using the Draize scoring method (Wen et al., 2012). Erythema and edema, the two primary skin parameters that were evaluated, were visually assessed and scored from 0–4. The reaction scores for erythema and edema were added together and divided by two to calculate the primary skin irritation index. The grouping information is shown in Table 1.

Statistical analysis
Data are expressed as the mean ± standard deviation (SD). One-way analysis of variance followed by Dunnett’s post hoc test for statistical comparisons was performed using GraphPad Prism 5.0 (GraphPad Software, Inc., San Diego, CA, USA).

Results
Morphology and growth patterns of DRG neurons
Collected DRG explants containing DRG neurons and the surrounding Schwann cells were immunostained with both the neuron marker β-tubulin and the Schwann cell marker S100. DRG neurons were able to spread and grow on both butterfly wings, but the cell growth rate and the diffusion directions differed depending on the surface structure morphologies of the butterfly wings. On M.m. wing surfaces, which feature grooves, cells grew along the longitudinal structural stripes (Figure 1). However, on P.u.t. wing surfaces, which feature micro-/nano-concave surfaces, cells grew randomly in all directions (Figure 1).

Morphology and growth patterns of Schwann cells
Because the dedifferentiation and proliferation of Schwann cells play significant roles in peripheral nerve regeneration (Steri et al., 2019), the proliferation of Schwann cells on M.m. wings was also examined. Schwann cells cultured on M.m. wings exhibited EDU-positive signals, indicating that Schwann cells were able to grow and proliferate on M.m. wings (Figure 3). Schwann cells were also cultured on P.u.t. wings and chitosan, which resulted in comparable proliferation rates (Figure 3).

In addition to cellular proliferation, the cellular adhesion conditions on M.m. wings, P.u.t. wings, and chitosan were examined. The attachments of proliferating Schwann cells to two species of butterfly wings and chitosan at different time points (1, 2, and 3 hours) were determined by culturing Schwann cells that express green fluorescent protein. Qualitative observation showed that similar as chitosan, Schwann cells could attach to M.m. wings and P.u.t. wings (Figure 4). DiO labeling also suggested that Schwann cells were able to adhere to M.m. wings, P.u.t. wings, and chitosan (Figure 5).

Biosafety of M.m. wings in vivo
The biosafety of butterfly wings in Sprague-Dawley rats was evaluated by examining the effects of the subcutaneous implantation of M.m. wings (including untreated and acid and base treated M.m. wings) into the backs of rats. Rats showed normal appetites and movement after the subcutaneous implantation of biomaterials. The wounds appeared red and swollen 1 and 2 days after surgery. These symptoms were alleviated with time, and no swelling or suppuration was observed at any time point.

Histological observations showed that, in Sprague-Dawley rats implanted with untreated M.m. wings, fibrous connective tissues could be observed wrapping around the implanted M.m. wing at 1 week after implantation. At 4 weeks after implantation, the numbers of fibrous connective tissues increased, whereas the numbers of infiltrated inflammatory cells decreased. At 16 weeks after implantation, fewer inflammatory responses were observed, and the untreated M.m. wings began to degrade. The degradation of untreated M.m. wings was more obvious 24 weeks after implantation (Figure 6).

Reduced amounts of fibrous connective tissues wrapping the biomaterial and reduced inflammatory cell infiltration were observed in Sprague-Dawley rats implanted with either treated M.m. wings or chitosan compared with rats implanted with untreated M.m. wings. In rats implanted with treated M.m. wings or chitosan, blood vessel growth and the degradation of biomaterials occurred at earlier time points than in rats implanted with untreated M.m. wings, suggesting that treated M.m. wings and chitosan induced mild local inflammatory responses and exhibited good compatibility with the surrounding tissues (Figure 6).
rats 4 weeks after the implantation of treated *M. m. *wings or chitosan, as well as from normal rats. Except for creatine, alkaline phosphatase, neutrophil percentage, and lymphocyte percentage, the other blood parameters of rats injected with treated *M. m. *wings or chitosan were generally consistent with those of normal rats (Table 2). The creatine levels in rats injected with either treated *M. m. *wings or chitosan were much lower than those in rats injected with normal saline, whereas the alkaline phosphatase levels in rats injected with treated *M. m. *wings or chitosan were much higher than those in rats injected with normal saline. These data indicated that implanted biomaterials may induce certain effects on the liver functions of treated animals. The neutrophil percentages increased in rats implanted with treated *M. m. *wings or chitosan, whereas the lymphocyte percentages decreased in rats implanted with treated *M. m. *wings or chitosan, indicating the complexity of biomaterial-induced immune responses.

**Systemic acute toxicity, reactions to intradermal injections, and skin sensitization to *M. m. *wings, in an *in vivo* study**

During the 72-hour observation period following intraperitoneal injection, no abnormal phenomena, including vomiting, diarrhea, convulsions, gait instability, or respiratory depression, were observed in any treated ICR mice. No toxic phenomena were observed in any of the ICR mouse groups (Table 1). The body weights of ICR mice slightly increased after 72 hours, and no significant differences were observed between *M. m. *wing extract-treated and normal saline-treated groups or between the two genders (Figure 7).

No skin reactions were detected, and the primary skin irritation index was evaluated for each animal, as previously described (Wen et al., 2012). All rabbits in the 3, 6, and 12 cm²/mL *M. m. *wing extract groups received scores of 0 (Table 1).

Any signs of erythema or edema were recorded and scored according to the order of severity. Guinea pigs treated with formaldehyde showed moderate erythema and mild-to-moderate edema (score = 6), whereas *M. m. *wing extract and saline did not trigger any symptoms of skin sensitization when applied to the skin of guinea pigs (score = 0, Table 1).

**Discussion**

The surface characteristics of biomaterials can influence cellular fates and cellular behaviors, including dedifferentiation, survival, proliferation, attachment, and migration (Stevens and George, 2005; Phillips et al., 2010; Zhou et al., 2013; Kloczko et al., 2015). Butterfly wings, which have delicate surface topological structures, were used as biomaterials to culture Schwann cells and treat peripheral nerve injury (He et al., 2018). In the current study, DRG explants showed diverse growth patterns when cultured on *M. m. *and *P. u. t. *wings, indicating that the surface morphologies of butterfly wings have clear guiding effects on the primary cell types found in the peripheral nervous system. *M. m. *wings, which encouraged the directional growth of Schwann cells and DRG explants, may promote the dedifferentiation and migration of Schwann cells, as well as the elongation of axons, following peripheral nerve injury.

| Group | Intervention | Primary skin irritation index | Response |
|-------|--------------|-------------------------------|----------|
| Wing male (n = 7) | 6 cm²/mL butterfly wing extract buffer (50 mL/kg) | 0 | Without toxic symptoms in all four groups |
| Wing female (n = 7) | 6 cm²/mL butterfly wing extract buffer (50 mL/kg) | 0 | No erythema, edema in all four groups |
| Normal saline male (n = 7) | Normal saline (50 mL/kg) | 0 | No erythema, edema |
| Normal saline female (n = 7) | Normal saline (50 mL/kg) | 0 | No erythema, edema |
| Reaction test of intradermal injection (white rabbits) | | | |
| 12 cm²/mL butterfly wing extract buffer (n = 3, 12 cm²/mL butterfly wing extract buffer (0.2 mL/point) left 5 points/rabbit) | 0 | No erythema, edema |
| 6 cm²/mL butterfly wing extract buffer (n = 3, 6 cm²/mL butterfly wing extract buffer (0.2 mL/point) left 5 points/rabbit) | 0 | No erythema, edema |
| 3 cm²/mL butterfly wing extract buffer (n = 3, 3 cm²/mL butterfly wing extract buffer (0.2 mL/point) left 5 points/rabbit) | 0 | No erythema, edema |
| Normal saline (n = 9, right 5 points/rabbit) | Normal saline (0.2 mL/point) | 0 | No erythema, edema |
| Skin sensitization test (guinea pigs) | | | |
| 12 cm²/mL butterfly wing extract buffer (n = 8) | 0 | No erythema, edema |
| 6 cm²/mL butterfly wing extract buffer (n = 8) | 0 | No erythema, edema |
| Positive control (n = 8) | 4% formalin (0.1 mL/point) | 6 | Erythema, edema |
| Negative control (n = 8) | Normal saline (0.1 mL/point) | 0 | No erythema, edema |

**Table 2** | Serological effects of butterfly wings and chitosan on Sprague-Dawley rat 4 weeks after implantation

| Parameter | *M. m. *wings | Chitosan | Normal |
|-----------|---------------|---------|--------|
| Alanine aminotransferase (IU/L) | 49.00±2.16 | 45.66±3.68 | 42.00±3.26 |
| Aspartate aminotransferase (IU/L) | 120.30±6.55 | 109.33±9.39 | 137.00±22.70 |
| Blood urea nitrogen (mM) | 6.77±0.47 | 6.99±0.31 | 6.45±0.73 |
| Creatinine (µM) | 20.90±1.18 | 22.70±2.41 | 29.30±1.76 |
| Uric acid (µM) | 63.67±4.64 | 55.33±5.73 | 62.33±3.30 |
| Lactate dehydrogenase (IU/L) | 535.30±55.43 | 520.00±74.31 | 715.70±131.37 |
| Alkaline phosphatase (IU/L) | 307.33±7.76 | 292.00±10.03 | 224.33±23.44 |
| Creatine phosphokinase (IU/L) | 1374.00±204.71 | 1323.30±492.9 | 1297.30±805.9 |
| White blood cells (×10³/L) | 9.72±0.10 | 10.60±0.23 | 0.51±0.15 |
| Neutrophil percentage | 36.00±4.63 | 39.10±2.60 | 10.50±1.50 |
| Lymphocyte percentage | 52.70±10.61 | 52.57±7.21 | 84.27±3.39 |

Except for creatine, alkaline phosphatase, neutrophil percentage, and lymphocyte percentage (*P* < 0.05), the other blood parameters of rats injected with treated *M. m. *wings or chitosan were generally consistent with those of normal rats. Data are expressed as the mean ± SD and analyzed by one-way analysis of variance with Dunnett’s post hoc test. Experiments were conducted three times. *M. m.:* Morpho menelaus.
tests after implantation, acute toxicity tests, and histochemical examinations. The local reaction experiments use implanted materials. Our data showed that the implantation of butterfly wings, particularly M.m. wings, resulted in comparable effects as chitosan in regard to cell proliferation and attachment. These results further demonstrated the biocompatibility of butterfly wings.

Synthetic materials that feature directional lines could also guide the growth of neurons, as shown previously (Bain et al., 2016). Synthetic materials that feature directional lines at various intervals resulted in differing effects on cell growth. The parallel ridges found on M.m. wings were spaced approximately 2 µm apart, which is a much narrower interval than can be found in most artificial materials. We compared the effects of a chitosan membrane with 30 µm parallel ridges with the effects of M.m. wings and found that M.m. wings appear to be more suitable for the growth of Schwann cells and neurons (unpublished data), indicating the importance of topological structures for cellular behaviors.

In addition to Schwann cell migration and proliferation, the influence of biomaterials on cell dedifferentiation was previously investigated using transcriptome-based network analysis (He et al., 2018). The expression levels of dedifferentiation-associated genes, including Mtor (mechanistic target of rapamycin kinase), Zfp580 (zinc finger protein 580), Jun (Jun proto-oncogene, AP-1 transcription factor subunit), Cacna1g (calcium voltage-gated channel subunit alpha1g), Cdk6 (cyclin-dependent kinase 6), Ncoa3 (nuclear receptor coactivator 3), and Mif (macrophage migration inhibitory factor) were examined and compared between cells grown on M.m. wings and cells grown on P.u.t. wings. Sequencing data showed that the expression levels of these dedifferentiation-associated genes were elevated in cells seeded on M.m. wings compared with the levels of these genes in cells seeded on P.u.t. wings 0.5, 1, and 3 hours after cell culture (He et al., 2018).

Additionally, in vivo studies have previously been conducted to study the biosafety of using butterfly wings as biomaterials as the foundation of constructed tissue-engineered products (Orabi et al., 2013; Sun et al., 2015; Croissant et al., 2018). Several in vivo biosafety examinations, including local reaction tests after implantation, acute toxicity tests, intradermal reaction tests, and skin sensitization tests, have been performed, similar to those described in the present study. The local reaction experiments use in vivo implantation technology to evaluate the biological responses to materials (Sigler et al., 2005; Kuznetsova et al., 2014; Velnar et al., 2016). Histological indicators, including the numbers and distributions of inflammatory cells, fibrosis or the formation of a fibroelastic cavity, and the existence of material debris, are employed to evaluate the toxicity and degradation of implanted materials. Our data showed that the implantation of M.m. wings did not induce redness, induration, or necrosis of the skin on the back of Sprague-Dawley rats. Hematoxylin-
in rats implanted with treated M.m. wings began to degrade, which became increasingly apparent 24 weeks after implantation. Moreover, the arrows indicate implanted biomaterials. Scale bars: 50 µm. Experiments were conducted three times. Chitosan exhibited mild local inflammatory responses and good compatibility with surrounding tissues. Treated M.m. wings or M.m. of biomaterials were observed at earlier time points than with untreated wings. Treated M.m. wings. At 16 weeks after implantation, the untreated M.m. and the rats, compared with untreated M.m. wings. At 16 weeks after implantation, the untreated M.m. wings began to degrade, which became increasingly apparent 24 weeks after implantation. Moreover, in rats implanted with treated M.m. wings or chitosan, the growth of blood vessels and the degradation of biomaterials were observed at earlier time points than with untreated wings. Treated M.m. wings or chitosan exhibited mild local inflammatory responses and good compatibility with surrounding tissues. The arrows indicate implanted biomaterials. Scale bars: 50 µm. Experiments were conducted three times. M.m.: Morpho menelaus; P.u.t.: Papilio ulysses teleogenus.

Figure 4 | The adhesion of Schwann cells on M.m. and P.u.t. wings. The adhesion conditions of Schwann cells cultured on M.m. wings, P.u.t. wings, and chitosan, 1, 2, and 3 hours after cell seeding. An increased number of Schwann cells attached effectively to butterfly wings during the early culture. Data are expressed as the mean ± SD and were analyzed by one-way analysis of variance with Dunnett’s post hoc test. Scale bars: 50 µm. Experiments were conducted five times. M.m.: Morpho menelaus; P.u.t.: Papilio ulysses teleogenus.

Figure 5 | The attached Schwann cells on M.m. and P.u.t. wings after 6-hour culture. Schwann cells labeled with DiO were able to survive and grow on both M.m. and P.u.t. wings, after 6 hours. Scale bars: 100 µm. Experiments were conducted three times. DiO: 3,3′-Dioctadecyloxacarbocyanine perchlorate; M.m.: Morpho menelaus; P.u.t.: Papilio ulysses teleogenus.

Figure 6 | Pathological changes after M.m. wings were implanted in the backs of Sprague-Dawley rats (hematoxylin-eosin staining). Untreated M.m. wings (A–D), acid and base treated M.m. wings (E–H), and chitosan (I–L) were subcutaneously implanted into Sprague-Dawley rats. Reduced fibrous connective tissue wrapping and inflammatory cell infiltration were observed when treated M.m. wings or chitosan was implanted into the rats, compared with untreated M.m. wings. At 16 weeks after implantation, the untreated M.m. wings began to degrade, which became increasingly apparent 24 weeks after implantation. Moreover, in rats implanted with treated M.m. wings or chitosan, the growth of blood vessels and the degradation of biomaterials were observed at earlier time points than with untreated wings. Treated M.m. wings or chitosan exhibited mild local inflammatory responses and good compatibility with surrounding tissues. The arrows indicate implanted biomaterials. Scale bars: 50 µm. Experiments were conducted three times. M.m.: Morpho menelaus.

Figure 7 | Body weights of ICR mice after butterfly wing extract injection. The body weight of mice was measured at 24, 48, and 72 hours after injection. There were no significant differences between the treated and untreated groups. M.m. and the degradation of biomaterials or severe inflammatory responses. The observation of blood vessel growth and the degradation of biomaterials indicated that the implanted M.m. wings were non-toxic, degradable, and bioactive.

The acute toxicity test is a routine biosafety testing method that examines the influences of biomaterials on organism metabolism and safety (Misik et al., 2015; Hu et al., 2018). ICR mice injected with M.m. wing extracts showed no adverse reactions. An increasing trend in body weights was observed among M.m. wing extract-injected mice. These outcomes indicated the safety of M.m. wings for potential clinical applications.

Additionally, an intradermal reaction test was conducted in rabbits because rabbits tend to have sensitive responses (Gisquet et al., 2011; Diao et al., 2013). A skin sensitization test was conducted using guinea pigs because guinea pigs present a similarly delayed hypersensitivity as that observed in humans (Robinson et al., 1990; Basketter et al., 2008; Basketter et al., 2015). Similar to animals treated with normal saline, no edema, erythema, or other pathological immune responses were detected in animals treated with M.m. wing extracts, demonstrating that M.m. wing extracts do not contain allergens. However, one weakness of our current study was that we only tested 4% formalin as a positive control in the skin sensitization test but did not use formalin as a positive control for acute toxicity because it may greatly damage the animals. The effects of 4% formalin should also be tested in the systemic acute toxicity test and reaction test of intradermal injection.

Although butterfly wings exhibited good in vitro biocompatibility with Schwann cells and DRG neurons and good in vivo histocompatibility and biosafety, barriers to the use of butterfly wings in clinical applications still exist. Currently, unlike chitosan, obtaining sufficient amounts of butterfly wings for large scale clinical use may be difficult, which may limit the commercial application of butterfly wings as a biomaterial. However, our current study provided a detailed and reliable experimental basis for future research into bio-mimicking materials for use in neural tissue engineering and regenerative medicine applications.

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References

Bain LE, Kistre R, Johnson CA, Ghagshheir HT, Collazo R, Ivanisevic A (2016) Neurotrophic cell attachment and growth on III-nitride lateral polarity structures. Mater Sci Eng C Mater Biol Appl 58:1194-1198.

Basketter D, Darlenski R, McFlwr JW (2008) Skin irritation and sensitization: mechanistic and new approaches for risk assessment. Skin Pharmacol Physiol 21:191-202.

Basketter D, White IR, McFadden JP, Kimber I (2015) Hexyl cinnamal: skin absorption and irritation. Environ Health Perspect 123:245-249.

Basketter D, Fluhr JW (2008) Skin irritation and sensitization: mechanistic and new approaches for risk assessment. Skin Pharmacol Physiol 21:191-202.

Bhat NK, Khan TR, Meijias C, Paniello RC (2017) Nerve transaction repair using laser-activated chitosan in a rat model. Lasersurgery 127:E253-257.

Croissant JG, Fatieiev Y, Almalik A, Khashab NM (2018) Mesoporous silica and organosilica nanoparticles: physical chemistry, biosafety, delivery strategies, and biomedical applications. Adv Healthc Mater 7:1708031.

Croisio A, Fornasari BE, Gambarrreta G, Geuna S, Raimondi S, Battiston B, Tos P, Rosini G (2019) Chitosan tubes enriched with fresh skeletal muscle fibers for delayed repair of peripheral nerve defects. Neuro Reports 41:1079-1084.

Diao JS, Xia WS, Yi CG, Yang Y, Zhang X, Xia W, Shu MG, Wang YM, Gu L, Guo S (2013) Histone deacetylase inhibitor reduces hypertrophic scarring in a rat model. Plast Reconstr Surg 132:61e-69e.

Dietzmeyer N, Förthmann M, Grothe C, Haastert-Talini K (2020) Modification of tubular chitosan-based peripheral nerve implants: applications for simple or more complex approaches. Neuro Reports 41:1421-1431.

Elbaz A, Lu J, Zhou Y, Zhang G, Liu H, Blondel WC, Leroux A, Latarche C, Merlin JL, Chassagne G (2019) Bio mimicking of myelin formation by combined high affinity with extracellular matrix structure of electrospun silk fibroin nanoscaffolds. J Biomater Sci Polym Ed 30:1068-1082.

Facklam AL, Volpatti LR, Anderson DG (2020) Biomaterials for personalized tissue engineered and regenerative medicine products. Trends Biotechnol 38:911-917.

Fragg S, Tackel TE, Almalik A, Khashab NM (2018) Mesoporous silica and organosilica nanoparticles: physical chemistry, biosafety, delivery strategies, and biomedical applications. Adv Healthc Mater 7:1708031.

Haastert-Talini K (2020) Modification of tubular chitosan-based peripheral nerve implants: applications for simple or more complex approaches. Neuro Reports 41:1421-1431.

Habib H, Bouthou M, Morissette A, Rousseau A, Chabaud S, Bolduc S (2013) Tissue engineering of urinary bladder and urethra: advances from bench to patients. Sci Technol World 2013:145564.

Park EJ, Lee GH, Yoon C, Jeong U, Kim Y, Cho MH, Kim DW (2016) Biodistribution and toxicity of spherical aluminum oxide nanoscaffolds. J Appl Toxicol 36:424-433.

Phillips JE, Petrie TA, Creighton FP, Garcia AJ (2010) Human mesenchymal stem cell differentiation on self-assembled monolayers presenting different surface chemistries. Acta Biomater 6:12-20.

Qian Y, Zhou X, Zhang F, Diekwisch TG, Luan X, Yang J (2019) Triple PLGA/PCL scaffold modification including silver impregnation, collagen coating, and electrosprining significantly improve biocompatibility, antimicrobial, and osteogenic properties for orofacial tissue regeneration. ACS Appl Mater Interfaces 11:37381-37396.

Robinson MK, Nusair TL, Fletcher ER, Ritz HL (1990) A review of the Buehler guinea pig skin sensitization test and its use in a risk assessment process for human skin sensitization. Toxicology 61:97-107.

Sgier M, Paul T, Grabitz RG (2005) Biocompatibility screening in cardiovascular implants. Z Kardiol 94:383-391.

Stenberg L, Kodama A, Lindwall-Blom C, Dahlin LB (2016) Nerve regeneration in chitosan conduits and in autologous nerve grafts in healthy and in type 2 diabetic Goto-Kakizaki rats. Eur J Neurosci 43:463-473.

Stevens MM, George JH (2005) Exploring and engineering the cell surface interface. Science 310:1135-1138.

Sterielli S, Imperatore V, Lloyd AC (2019) Schwann cell plasticity-roles in tissue homeostasis, regeneration, and disease. Glia 67:2203-2215.

Sun LC, Su Y, Ding X, Xu DS, Li CM, Wang L, Li WL, Sun XD, Yu JM, Meng X (2020) Methods for delayed repair of peripheral nerve defects. Neuro Reports 41:1079-1084.

Sun X, Dai H, Guo P, Sha X (2019) Biocompatibility of a new kind of polyvinyl alcohol embolic microspheres: in vitro and in vivo evaluation. Mol Biotechnol 61:610-621.

Sun Y, Feng W, Yang P, Huang C, Li F (2015) The biosafety of lanthanide upconversion nanomaterials. Chem Rev 44:1509-1525.

Velnar T, Bunc G, Kobucar R, Gradinsik L (2016) Biomaterials and host versus xenograft response: a short review. Bosn J Basic Med Sci 16:82-90.

Vermeulen S, de Boer J (2020) Screening as a strategy to drive regenerative medicine research. Methods doi:10.1016/j.meth.2020.04.004.

Wang X, Hu W, Cao Y, Hao J, Wu J, Gu X (2005) Dog sciatic nerve regeneration across a 30-mm defect bridged by a chitosan/PGA artificial nerve graft. Brain Res 1289:1897-1910.

Wen MM, El-Kamel AH, Khalil SA (2012) Systemic enhancement of papaverine transdermal gel for erectile dysfunction. Drug Dev Ind Pharm 38:912-922.

Yu S, Xu L, Gu X (2019) Scaffolds for peripheral nerve repair and reconstruction. Exp Neurol 319:112761.

Yu HD, Zhang L, Liu YX, Mao M, XN XB, Leng WD, Lio J (2020) Construction and characterization of nano-hydroxyapatite/chitosan/polycaprolactone composite scaffolds by 3D printing. Zhongguo Zuzhi Gongcheng Yanjiu 129:214-230.

Zhang W, Zhang D, Deng T, Shang W (2015) Infrared detection based on tubular chitosan-based peripheral nerve implants: applications for simple or more complex approaches. Neuro Reports 41:1421-1431.

Zhou J, Sui F, Yao M, Wang Y, Liu Y, Tian F, Li Q, He X, Sha L, Liu Z (2013) Novel nanomaterial scaffolds regulate the biological behaviors of neural stem cells. Neuro Reports 41:1089-1092.

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