Breast cancer remains a major cause of cancer death in women in the developed world. Novel therapeutic modalities are needed for those patients in whom chemotherapy, hormonal treatment and external radiation therapy are ineffective. 2-Deoxy-2-[18F]fluoro-D-glucose (18F-FDG) is widely used in positron emission tomography (PET) for the evaluation of patients with tumors [1,2]. It was shown by Warburg in 1930 that glucose is actively utilized by tumor cells [3]. In recent years the use of 18F-FDG-PET has become well established in the diagnosis of breast cancer, because many breast cancers demonstrate high avidity for 18F-FDG [4], which is an analogue of glucose in which the hydroxy group in the 2 position has been replaced with a fluorine atom. 18F-FDG is taken up by the cells and phosphorylated by hexokinase to 18F-FDG-6-

**Abstract**

**Background:** Novel approaches are needed for breast cancer patients in whom standard therapy is not effective. 2-Deoxy-2-[18F]fluoro-D-glucose (18F-FDG) was evaluated as a potential radiomolecular therapy agent in breast cancer animal models and, retrospectively, in patients with metastatic breast cancer.

**Methods:** Polyoma middle T antigen (PyMT) and mouse mammary tumor virus-NeuT transgenic mice with tumors 0.5–1 cm in diameter were imaged with 18F-FDG, and tumor to liver ratios (TLRs) were calculated. The radiotoxicity of 18F-FDG administration was determined in healthy mice. PyMT mice with small (0.15–0.17 cm) and large (more than 1 cm) tumors were treated with 2–4 mCi of 18F-FDG, and control C3H/B6 mice with 3 mCi of 18F-FDG. At 10 days after treatment the tumors and control mammary glands were analyzed for the presence of apoptotic and necrotic cells. Five patients with breast cancer and metastatic disease were evaluated and standardized uptake values (SUVs) in tumors, maximum tolerated dose, and the doses to the tumor were calculated.

**Results:** Doses up to 5 mCi proved to be non-radiotoxic to normal organs. The 18F-FDG uptake in mouse tumors showed an average TLR of 1.6. The treatment of mice resulted in apoptotic cell death in the small tumors. Cell death through the necrotic pathway was seen in large tumors, and was accompanied by tumor fragmentation and infiltration with leukocytes. Normal mammary tissues were not damaged. A human 18F-FDG dose delivering 200 rad to the red marrow (less than 5% damage) was calculated to be 4.76 Ci for a 70 kg woman, and the dose to the tumors was calculated to be 220, 1100 and 2200 rad for SUVs of 1, 5 and 10, respectively.

**Conclusion:** We have shown that positrons delivered by 18F-FDG to mammary tumors have a tumoricidal effect on cancer cells. The study of breast cancer patients suggests that the tumor and normal organ dosimetry of 18F-FDG makes it suitable for therapy of this malignancy.

**Keywords:** breast cancer, 2-deoxy-2-[18F]fluoro-D-glucose, mouse models, positrons, therapy

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Introduction

Breast cancer remains a major cause of cancer death in women in the developed world. Novel therapeutic modalities are needed for those patients in whom chemotherapy, hormonal treatment and external radiation therapy are ineffective. 2-Deoxy-2-[18F]fluoro-D-glucose (18F-FDG) is widely used in positron emission tomography (PET) for the evaluation of patients with tumors [1,2]. It was shown by Warburg in 1930 that glucose is actively utilized by tumor cells [3]. In recent years the use of 18F-FDG-PET has become well established in the diagnosis of breast cancer, because many breast cancers demonstrate high avidity for 18F-FDG [4], which is an analogue of glucose in which the hydroxy group in the 2 position has been replaced with a fluorine atom. 18F-FDG is taken up by the cells and phosphorylated by hexokinase to 18F-FDG-6-
phosphate. Because $^{18}$F-FDG is not a substrate for glycolysis and does not undergo further metabolism, it remains trapped in the cell [5].

$^{18}$F emits positrons with an average energy of 0.250 MeV and abundance of 96%. Positrons lose their kinetic energy in the tissue in the same manner as electrons, thereby damaging tissue. This is followed by annihilation, which results in the emission of two photons with an energy of 511 keV in opposite directions. Although the potential of electrons to kill cancer cells through the loss of their kinetic energy has been made use of in radionuclide cancer treatment for more than 50 years (since the introduction of therapy of thyroid cancer with $^{131}$I [6]), the therapeutic potential of positrons has remained unexplored. Theoretically, positrons should kill cancer cells during the loss of kinetic energy in the same manner as electrons.

Here we evaluate, for the first time to our knowledge, the potential of $^{18}$F-FDG as a positron-emitting agent for the radiomolecular therapy of breast cancer in breast cancer animal models and, retrospectively, in patients with metastatic breast cancer.

**Materials and methods**

**Animals**

All procedures involving mice were conducted in accordance with the National Institutes of Health regulations concerning the use and care of experimental animals. The study of mice was approved by the Albert Einstein College of Medicine Animal Use Committee. Transgenic mice expressing the polyoma middle T antigen (PyMT) in the mammary epithelium under the control of mouse mammary tumor virus (MMTV) long terminal repeat were provided by Dr WJ Muller (McMaster University, Ontario, Canada) and then bred in our institution. At the age of 10 weeks these mice have multiple mammary tumors 0.15–0.17 cm in diameter. In mice older than 18 weeks the tumors are more than 1 cm in diameter. MMTV-NeuT mice [7], which carry erbB-2 (Neu), one of the better known human breast cancer oncogenes, were purchased from Jackson Laboratories. MMTV-NeuT mice were obtained as retired breeders and some of them developed mammary tumors at the age of 5 months, whereas others remained-tumor free until 6–7 months of age. C3H/B6 female mice lacking the PyMT transgene were used as healthy controls in therapy experiments.

**Imaging of mice with $^{18}$F-FDG**

PyMT mice older than 18 weeks, with tumors more than 1 cm in diameter, MMTV-NeuT tumor-bearing mice (0.5–1 cm in diameter) and tumor-free MMTV-NeuT mice were fasted for 4 hours before the injection of radiotracer. Three animals were used in each group. They were anesthetized with a mixture of 125 mg/kg ketamine and 10 mg/kg xylazine. An injection of 0.5–2.0 mCi $^{18}$F-FDG was administered intraperitoneally (i.p.). The mice rested while anesthetized for an uptake period of 1 hour. A scan was performed on a dedicated PET scanner CPET (Philips). Scans (6 min emission and 45 s transmission) were obtained. The data were acquired with a zoom of 2 and a slice thickness of 2 mm. Images were reconstructed with an iterative reconstruction algorithm and corrected for attenuation. To reduce volume averaging, a small round region of interest 12 pixels in size was drawn in the center of the tumor and in the center of normal liver. The diameter of the region was 7 mm. The tumor to liver ratios (TLRs) were calculated by the formula TLR=counts per pixel in tumor divided by counts per pixel in liver.

**Radiotoxicity studies of $^{18}$F-FDG in healthy mice**

After a 4-hour fast, 2 groups of BALB/c mice were treated i.p. with the following doses of $^{18}$F-FDG: group 1 (three mice), 2.5 mCi; group 2 (three mice), 5 mCi; group 3 (three mice), left untreated for control. The mice were monitored for changes in behavior and body weight for 1 month, after which they were killed; their heart, brain, liver, kidneys, bladder, and bone marrow were removed, fixed in buffered formalin, sectioned, stained with hematoxylin and eosin (H&E), and analyzed histologically.

**Treatment of PyMT mice with $^{18}$F-FDG**

After a 4-hour fast, three groups of mice were treated i.p. with the following doses of $^{18}$F-FDG: group 1 (five 10-week-old mice), 2–4 mCi; group 2 (three 22-week-old mice), 2 mCi; group 3 (two C3H/B6 mice), 3 mCi to assess radiation damage to healthy breast tissue. Three 10-week-old and two 22-week-old PyMT mice served as untreated controls. At 10 days after treatment, mice were killed. In younger mice, the right abdominal mammary glands were removed for whole mount preparation as described [8], then fixed in buffered formalin and sectioned. In older mice, the tumors were removed and processed as above. Some sections were stained with H&E; others were analyzed for the presence of apoptotic and necrotic cells.

**Apoptosis and necrosis detection**

The detection of apoptotic and necrotic cells in the tumors was performed with an Apoptag Plus® apoptosis detection kit (Serologicals) in accordance with the manufacturer’s instructions. In brief, 3'-OH termini of DNA fragments, which are the hallmark of apoptosis, were labeled with digoxigenin-modified nucleotides by terminal deoxynucleotidyl transferase. This enzyme selectively detects apoptotic over necrotic cells. The labeled DNA was detected with an anti-digoxigenin antibody, and detection was performed with a chromagen: apoptotic cells were stained brown, and areas of necrosis were stained yellow.

**$^{18}$F-FDG-PET in breast cancer patients with metastatic disease**

Approval was obtained from the Albert Einstein College of Medicine Cancer Center Protocol Review Committee.
and the Montefiore Medical Center Institutional Review Board. Retrospectively, five consecutive patients with breast cancer and metastatic disease shown on ¹⁸F-FDG-PET scanning were evaluated. After more than 4 hours of fasting, the patients were administered 3.5 mCi of ¹⁸F-FDG, and rested during an uptake period of 45 min. The patients then underwent a whole-body scan on the CPET scanner. The scanning protocol consisted of 6 min of emission and two rotations of a ¹³⁷Cs source for transmission per bed position, and approximately six bed positions. Images were corrected for attenuation and reconstructed with the iterative method. To reduce volume averaging, a small round region of interest 12 pixels in size was drawn in the center of the tumor and in the center of normal liver. The diameter of the region was 14 mm. Standardized uptake values (SUVs) were calculated for all regions of interest by the formula SUV = (activity in tissue [mCi/g]) divided by (injected activity [mCi]/body weight [g]).

TLRs were calculated by the formula TLR = SUV of tumor divided by SUV of liver.

The dose-limiting organ for therapy with ¹⁸F-FDG is the bone marrow. The activity of ¹⁸F-FDG that will deliver doses of 200 rad to the red marrow (less than 5% damage in 5 years) [9] and also 300 rad were calculated using the Medical Internal Radionuclide Dosimetry formalism. A dose of 300 rad was considered because it causes acceptable and manageable hematologic toxicity in selected patients [9]. The subsequent doses delivered to ¹⁸F-FDG-avid tumors were calculated.

**Results**

**Uptake of ¹⁸F-FDG in mammary tumors of PyMT and MMTV-neuT mice**

Coronal PET images of PyMT and MMTV-neuT mice injected with ¹⁸F-FDG are presented in Figure 1. Slices (2 mm thickness) with the highest activity in the tumor were chosen. There was significant uptake of ¹⁸F-FDG by the tumors in PyMT (Fig. 1a,b) and MMTV-neuT mice (Fig. 1c). The tumor uptake was uniform. TLRs were (mean ± SD) 1.6 ± 0.4 and 1.6 ± 0.1 in MMTV-neuT and PyMT mice, respectively. No abnormal uptake was seen in a tumor-free mouse (Fig. 1d). As ¹⁸F-FDG is normally excreted in the urine, bladder activity was visible in all mice. The avidity of tumors for ¹⁸F-FDG provided an impetus for investigation of the therapeutic effect of ¹⁸F-FDG on mammary tumors in mice.

**Lack of radiotoxicity of ¹⁸F-FDG in normal mice**

Treatment of healthy mice with doses of up to 5 mCi ¹⁸F-FDG caused no damage in major organs (as determined by histological examination) including bone marrow, which is a dose-limiting organ in patients (results not shown).

**Tolerability of treatment of PyMT mice with ¹⁸F-FDG**

PyMT mice treated with 2–4 mCi ¹⁸F-FDG were observed for 10 days for obvious signs of radiation toxicity. At 24 h after injection no radioactivity was detected in mice because of the excretion and complete radioactive decay of the relatively short-lived isotope ¹⁸F (half-life 110 min). No changes in eating and drinking habits, urine and fecal excretion, or body weight were seen.

**Damage to the tumors by ¹⁸F-FDG**

Figure 2 shows microscopic images of small and large tumors from PyMT mice. The small (0.15–0.17 cm diameter) tumors from 10-week-old mice treated with ¹⁸F-FDG had numerous apoptotic cells clearly present in the center of the treated tumors (Fig. 2a) that were not detected in untreated tumors (Fig. 2b). Overall, 4 ± 1% of cells in the treated small tumors were apoptotic, in comparison with less than 1% in untreated tumors (P < 0.05). No apoptosis or necrosis was detected in the healthy mammary glands of C3H/B6 mice treated with 3 mCi of ¹⁸F-FDG (Fig. 2c). ¹⁸F-FDG treatment also caused much more cell death through the necrotic pathway in large (more than 1 cm) tumors in 22-week-old mice than occurred in untreated tumors (Fig. 2d,e). In the treated tumors, the areas occupied by necrotic cells were stained brown–yellow (Fig. 2d), as opposed to the sheets of bluish tumor cells in untreated controls (Fig. 2e). Necrotic areas constituted 14% of the tumor volume in 22-week-old mice. Some apoptotic cells were also visible at the rim of the necrotic area.

Figure 2f,g displays H&E-stained large tumors from 22-week-old PyMT mice. Tumors that had been treated with ¹⁸F-FDG were bloody when sectioned, which suggests resorption. This observation was confirmed by heavy infiltration of leukocytes in the H&E-stained section (Fig. 2f). Furthermore, the sections of the tumors treated with ¹⁸F-FDG showed a loss of coherence of the tumor cells with breaks in the epithelial sheets (Fig. 2f) as opposed to solid sheets of tumor cells found in the untreated controls (Fig. 2g).

**¹⁸F-FDG-PET in breast cancer patients with metastatic disease**

Table 1 summarizes the SUVs for metastatic tumors, SUVs for normal liver and TLRs in patients with metastatic breast cancer imaged with ¹⁸F-FDG. ¹⁸F-FDG-avid metastatic breast cancer in five retrospectively studied patients showed an average TLR of 2.7 ± 0.8. Figure 3 presents a ¹⁸F-FDG-PET projection image of a patient with breast cancer, metastatic to the right lung. A left lung metastasis was also seen. Normal activity in the heart, liver, kidneys, bladder, and bowel was observed. It should be also noted that the primary breast cancer had previously been resected, and the residual normal non-lactating breast tissue did not display increased ¹⁸F-FDG uptake.
over the background. The SUV within a tumor was uniform, because our patients did not display areas of necrosis in the tumors. In patients with multiple tumors the SUVs varied from site to site. In patient 5, the most intense SUV was 9.9 in the tumor with a diameter of 5 cm, and the least intense SUV was 2.9 in the tumor with a diameter of 1.5 cm. In patient 3, the SUV was 5.8 in the tumor with dimensions 10 cm × 6 cm × 4.5 cm, and the lowest SUV was 3.8 in the tumor with a diameter of 2 cm.

The activity of $^{18}$F-FDG to deliver 200 rad to the red marrow was calculated to be 4.76 Ci for a 70 kg woman, and the subsequent tumor doses were calculated to be 220, 1100, and 2200 rad for SUVs of 1, 5, and 10, respectively. The activity of $^{18}$F-FDG to deliver 300 rad to the red marrow was calculated to be 7.14 Ci, and tumor doses would be 330, 1650, and 3300 rad for SUVs of 1, 5, and 10, respectively. These doses are in the tumoricidal range.

Discussion

We have reported the use of positrons for the treatment of malignancy. Theoretically, these positrons can kill cancer cells in the same manner as electrons. However, the cytoidal potential of positrons remains largely unexplored. Historically, owing to the early success of the therapy of thyroid cancer with $^{131}$I, which emits electrons, much of the further development of radiopharmaceuticals for cancer therapy has concentrated on electron-emitting radioisotopes. The only reported use of the cytoidal potential of positrons was described by Stoll and colleagues [10], who used a balloon filled with the positron-emitter $^{68}$Ga for coronary artery brachytherapy to prevent restenosis.
Metabolic trapping of $^{18}$F-FDG is an attractive mechanism for delivering radioactivity to tumors, because neoplastic cells have an enhanced rate of glucose utilization [11]. This mechanism has been used successfully in $^{18}$F-FDG-PET, which is widely used in nuclear medicine for the diagnosis of oncological diseases. $^{18}$F-FDG has the ability to remain in cancer cells with low efflux rates. With a physical half-life of almost 2 hours, $^{18}$F emits energetic positrons with high abundance (96%) and a path length in tissue of about 0.1–0.2 cm. These qualities make $^{18}$F-FDG a potential candidate for investigation as an agent for the treatment of breast and other cancers.

Figure 2

Apoptosis and necrosis caused by treatment with $^{18}$F-FDG in mammary tumors in PyMT mice. Apoptotic and necrotic cells were detected with an Apoptag Plus apoptosis detection kit. (a) A treated tumor in a 10-week-old mouse has numerous apoptotic cells present (stained brown) in the center of the tumor. (b) An untreated tumor in a mouse of the same age has an insignificant number of apoptotic cells. (c) Healthy mammary glands of C3H/B6 mice treated with 3 mCi of $^{18}$F-FDG: no apoptotic or necrotic cells are present. (d) A treated tumor in a 22-week-old mouse shows extensive necrotic areas (stained brown–yellow); some apoptotic cells are also seen at the rim of the necrotic area. (e) An untreated tumor in a 22-week-old mouse. (f) An H&E-stained treated tumor in a 22-week-old mouse: heavy infiltration by leukocytes and a loss of coherence of the tumor cells with breaks in the epithelial sheets are observed. (g) An untreated tumor in a mouse of the same age shows solid sheets of tumor cells.

Original magnifications: (a–c) ×400; (d–g) ×200.

Table 1

| Patient | Diagnosis                        | SUV  | Normal liver | TLR  |
|---------|----------------------------------|------|--------------|------|
| 1       | Metastasis to sub-carinal lymph node | 5.3  | 2.8          | 1.89 |
| 2       | Metastasis to the left axilla     | 7.4  | 2.3          | 3.36 |
| 3       | Liver metastasis                 | 5.8  | 2.6          | 2.23 |
| 4       | Metastasis to the right axilla    | 5.3  | 2.1          | 2.52 |
| 5       | Right lung metastasis            | 9.9  | 2.7          | 3.67 |

SUVs were calculated for all regions of interest by the formula SUV = (activity in tissue [mCi/g] divided by (injected activity [mCi]/body weight [g]). TLRs were calculated by the formula TLR = SUV of tumor divided by SUV of liver.
Our imaging experiments in two different mouse mammary cancer models (the PyMT model of murine mammary cancer and the MMTV NeuT model, which carries the erbB-2 human breast cancer oncogenes) showed that it is possible to use these models for the investigation in vivo of the tumoricidal properties of positrons, because tumor uptake was demonstrated. We observed apoptosis and necrosis in tumors treated with 18F-FDG; particulate ionizing radiation is known to cause cell death through both the apoptotic [12] and necrotic pathways [13,14]. In small tumors (0.15–0.17 cm in diameter) in PyMT mice treated with 18F-FDG, the prevalent mode of cell death was apoptosis, whereas in large tumors (more than 1 cm in diameter) the radiation induced widespread necrosis. A possible explanation for this difference is that as the tumor diameter increased and there was an exponential increase of the absorbed radiation dose to the tumor, the high doses of radiation to the cell surface led to the focal stimulation of tumor necrosis factor-α expression [13] and a high influx of calcium [14], which induced necrosis instead of apoptosis. 18F-FDG at the 2–4 mCi doses that were used for the therapy of tumor-bearing animals contained 0.001–0.002 mg of unlabelled FDG, which should not cause any pharmacological effect because the level of glucose in the blood at fasting is 0.7 mg/ml (70 mg/dl).

A retrospective study of five patients with metastatic breast cancer imaged with 18F-FDG provided high SUVs in the tumors (2.7 ± 0.8). In patients with multiple tumors the SUVs varied from site to site. The tumors with greater uptake of the non-metabolite are affected more than the tumors with less uptake during positron therapy. The SUV of small tumors might suffer from volume averaging in measurement, and these tumors might actually receive a higher dose to the tumor than was measured. The dose-limiting organ for 18F-FDG administration is the red marrow. Other normal tissues show high 18F-FDG uptake, but they are relatively radioresistant. There are methods to reduce uptake by normal tissue. Uptake by cardiac and skeletal muscle is routinely reduced by fasting, and uptake by skeletal muscle can be further reduced with benzodiazepine therapy [15]. Uptake by brain is impossible to avoid. With an administered dose of 7.14 Ci of 18F-FDG, the dose to the brain is 570 rad. In external beam brain radiation therapy, 5040 rad is given in 28 fractions of 180 rad each, accompanied by corticosteroid therapy to decrease brain inflammation and edema [16]. The 18F-FDG therapy dose can be also be fractionated and corticosteroids can be administered to prevent toxicity to the brain. The dose to the bladder and kidneys can be reduced with a Foley catheter and diuretic administration [17]. These data suggest that 18F-FDG therapy can be used safely in 18F-FDG-avid malignancies.

With regard to long-term toxicity from positron therapy, it has been shown that after large cumulative doses of 131I for metastatic thyroid cancer, the risk of secondary leukemia is 0.4 deaths per 10^4 patient-year-grams [18]. We would expect patients with metastatic breast cancer treated with high doses of FDG to have a similar risk for latent leukemia. Patients who require whole-brain radiation therapy generally do not live long enough to attain a secondary malignancy, and there are no data on this.

One other possible advantage of using 18F-FDG as a therapeutic agent in breast cancer is that up to 29% of glucose utilization in the tumor is due to uptake in non-neoplastic cells, mostly macrophages [19]. In a mouse model it has been shown that macrophages contribute to tumor progression and metastasis [20]. In a mouse model it has been shown that macrophages contribute to tumor progression and metastasis [20]. Thus, treatment with 18F-FDG of metastatic breast cancer with poor prognosis could be particularly suitable because the macrophages are targeted in addition to the tumor cells.

We can envisage the application of other positron-emitters that have longer half-lives and emit higher-energy positrons than those emitted by 18F for positron tumor therapy. For example, 76Br-labeled bromo-D-glucose [21] could potentially deliver a higher radiation dose to the tumor because 76Br has a longer half-life (16.2 hours) than 18F and emits positrons with an energy of 3.44 MeV. Other compounds of interest for positron tumor therapy might include 124I-labeled iododeoxyuridine (half-life 4.2 days, energy 2.13 MeV), which incorporates into the DNA of

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**Figure 3**

18F-FDG-PET projection image of a patient with breast cancer metastatic to the right lung. A metastasis to the left lung is also visible. Normal activity is observed in the heart, liver, kidneys, bladder, and bowel. The primary breast cancer had previously been resected, and the residual normal non-lactating breast tissue did not display increased 18F-FDG uptake over the background.

![Figure 3](image-url)
cancer cells, and $^{64}$Cu-pyruvaldehyde bis(N-methylthiolsemicarbazone) (half-life 12.7 hours, energy 0.657 MeV) for the treatment of hypoxic tumors.

**Conclusion**

We have shown, to our knowledge for the first time, that positrons delivered by $^{18}$F-FDG to mammary tumors in mice cause apoptosis and necrosis of breast cancer cells. The dosimetry of $^{18}$F-FDG for tumors and normal organs in breast cancer patients suggests that $^{18}$F-FDG is a candidate for the radiomolecular therapy of refractory breast cancer and other cancers.

**Competing interests**

None declared.

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**Correspondence**

Ekaterina Dadachova PhD, Albert Einstein College of Medicine, Department of Nuclear Medicine, 1695A Eastchester Road, Bronx, NY 10461, USA. Tel: +1 718 405 8485; fax: +1 718 405 8457; e-mail: edadacho@aecm.yu.edu

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