Denoising of MRI images using fast NLM

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ABSTRACT
Denoising of image is a very crucial step which should retain fine details but should remove noise. Making the difference between noise and actual edge related data is very difficult. NLM filter helps to make a differentiation between image data and noise data. Its weight function decides the weightage of the neighboring pixel depending upon the similarity with the pixel to process. It helps to retain the edges and avoid it from smoothening. This paper discusses the implementation of NLM filter using hardware platform Spartan 6. After implementation of this on FPGA, not only denoise the image but preseve edges and there is a tremendous saving in time compared to its matlab implementation. Denoised image performance is calculated using various objective metrics such as MSE, PSNR, SSIM, PFOM etc. FPGA implementation shows clearly the advantages over its matlab implementation.

Keywords:
MSE
NLM
PFOM
PSNR
SSIM

1. INTRODUCTION
Medical imaging became an integral part of disease diagnosis in present days. Various medical modalities are available depending upon the application. The use of this modalities is to produce the clear imaging of anatomical structure within the body helping us to diagnose the malfunctioning of the body. The popular modalities available are X-rays, Computed Tomography, Nuclear imaging, Magnetic Resonance Imaging and Ultrasound to diagnose the various diseases. However, the common problem associated with all these modality while imaging is noise. Due to this noise, the intensity values in the image will vary from its original i.e. noise produces unwanted changes in the medical images leading to misdiagnosis. Noise is not introduced only while capturing the image but it also introduces while transmission, compression etc. Various factors are responsible for introduction of this noise in the resulting image. Every modality is affected by a different type of noise such as Nuclear imaging and X-rays are affected by quantum noise, Magnetic resonance imaging is affected by Rician noise, ultrasound imaging by speckle noise etc. This ultimately decreases the image contrast and misleads in diagnostic phase. So denoising is very important step to remove the noise from medical images [1].

Magnetic Resonance Imaging is a useful imaging technique to provide precise detailed images of internal organs and tissues in the human body. Nuclear Magneic resonance (NMR) is the main working principle of MRI system. It uses the concept of there is change in the nuclear spin when a specific proton or nuclei is kept in the magnetic field. By capturing this spin and by mapping it to spatial location MRI image is formed. Human body has 80% of water content and water is formation of hydrogen and oxygen. When hydrogen atoms are placed in strong magnetic field and excited by the resonant magnetic excitation pulse, there is change in the spin and when the excitation is removed then atom will return back to its original spin while radiating the waves. These waves are imaged to demonstrate the abnormal changes into human tissues [2].
MRI is having a limitation of limited aquisition time based on the patient’s comfort. This leads to low SNR of the MR images. The qualities of the magnetic resonance images are generally degraded with several artifact and noises that is adequately modeled as Rician noise. In the Rician noise model, the observed MR image intensities are non-linear function of the true image intensities and it is signal dependent noise and this adds bias to the medical images denoised by conventional denoising methods. So, a method which will remove noise from the image whereas will retain the structural fine details is a very important step in MR image denoising. While designing the algorithm for the denoising of MRI the main objective in front of many researches to provide images with both high SNR and good spatial resolution. Several filtering methods have been developed in the past decades to address denoising problem in MR images [3].

1.1. Previous Work Done

Denoising methods in MRI can be categorized in two groups: acquisition-based noise reduction and post acquisition-based noise reduction methods. The method for improving the signal to-noise ratio during the acquisition of an image is either increasing acquisition time or decreasing spatial resolution. However, the acquisition time is limited due to system throughput and patient comfort. Therefore, in acquisition-based method, there is a practical limit on the signal-to-noise ratio of the acquired MRI data. Hence, post acquisition image denoising is an inexpensive and effective alternative. The main objective of a post processing MRI denoising algorithm is reducing the noise power and maintaining the original resolution of the useful features in magnetic resonance images. In literature part, surveys of post acquisition-based noise reduction methods are explained [4].

Karl Krissian et al. [5] depicted Noise-Driven Anisotropic Diffusion Filtering of MRI. This method of filtering is proposed to remove the Rician noise from magnetic resonance images. It combines a Linear Minimum Mean Square Error filter and anisotropic diffusion filter (ADF).

The classic bilateral filter by Tomasi and Manduchi [6] is a weighted Gaussian filter that makes use of an intensity component in addition to the spatial component to reweight the Gaussian filter. Even though various methods for accelerating the original bilateral filter exist, it does not seem to be feasible to directly speedup the joint bilateral filtering. On the other hand, the bilateral filter is essentially a smoothing filter. It does not sharpen edges. The edge rendered by the bilateral filter has the same level of blurriness as in the original degraded image, although the noise is greatly reduced. The results of the bilateral filtering are a significant improvement over a conventional linear low-pass filter.

Non local mean algorithm takes a mean of all pixels in the image, weighted by how similar these pixels are to the target pixel. This results in much greater post-filtering clarity, and less loss of detail in the image compared with local mean algorithms [7].

All these methods introduced in the literature for removing noise from the image are computationally very complex and as image size goes on increasing, task becomes time consuming. A hardware approach to reduce the execution time of the filter is to use the multiprocessor architectures while porting the algorithm to parallel domain. With high end parallel architectures the speed up achieved is incomparably higher than the algorithmic solutions. But disadvantage of these mainframe architectures is they are costly and not programmer friendly. To make estimation of noise present in image and for removal of the same using complex algorithm is a crucial task which requires high computing capacity. In this context, hardware acceleration is crucial and Field programmable Gate Array (FPGA) best fit the growing demand of computational capabilities [8-16].

I P Skirnevskiy discuss short description of a parallel computing technology and its usage in different areas. He also provides comparison of the performance with and without using parallel computing as well as with different percentage of using CPU and parallel computing [17].

Handling the digital image processing with the help of conventional computer is accomplished only at the cost of time and conceptual distraction. Use of parallel processing for implementation of this algorithm helps us a lot [18-25].

1.2. The Proposed Work

The research work proposed here implements the non local mean filter using FPGA, for denoising brain MR images. The purpose of this work is to remove the Rician noise present in the MR image in much effective way in real time. FPGA used for this purpose is Spartan 6. Filter is implemented using VHDL language and ported on the kit.

2. RESEARCH METHOD

Consider $f$ as the noisy image and $h$ is the filtering parameter which is directly dependent on the standard deviation of noise. The estimated value of $i^{th}$ pixel using NLM filter is
\[ NL(f)(i) = \sum_{j \in I} w(i,j) f(j) \]  

where \( w(i,j) \) depend on the similarity between the pixel \( i \) and \( j \) and it is between 0 to 1 and \( \sum_j w(i,j) = 1 \). The similarity between the two pixel \( i \) and \( j \) depend on the similarity of intensity gray level vectors \( f(N_i) \) and \( f(N_j) \) where \( N_k \) denotes the square neighborhood of fixed size and centered at pixel \( k \). This similarity is measured as a decreasing function of the weighted Euclidean distance, \( \| f(N_i) - f(N_j) \|^2 \) where \( a > 0 \) is the standard deviation. Pixel with similar gray level will have more weight and pixel with different gray level will have less weight. This weight \( w(i,j) \) is calculated as

\[ w(i,j) = \frac{1}{z(i)} e^{-\frac{\| f(N_i) - f(N_j) \|^2}{2a^2}} \]

where \( z(i) \) is the normalizing constant and it is given by

\[ z(i) = \sum_j e^{-\frac{\| f(N_i) - f(N_j) \|^2}{2a^2}} \]

So for every pixel \( v(i) \) from noisy, on a defined neighborhood \( N_k \), non local mean filter will find out the weight for every pixel depending upon the similarity between the pixel to process and the pixel in the surrounding. This filter produces very promising result compared other traditional filters but the problem associated with this filter is that this filter is computationally very intensive. So for denoising complete image of size \( (I, J) \), it takes time. So result will be available after some time depending upon the size of image and the neighbourhood defined. To perform the fast computation of the said filter, hardware is useful. So we have implemented the said algorithm on FPGA platform which increases the speed of computation using parallel processing. This algorithm is implemented on Spartan 6 development board with device XC6SLX9 and it is compared with conventional NLM. The block diagram of proposed design is as shown in Figure 1.

Input image is applied pixel by pixel to FPGA for applying NLM algorithm. Inside the FPGA a specialized memory(SM) is designed to store the pixels received from the image. If \( I \) is the input image and \( f^{(N)}(i,j) \) is the estimation of \( i^{th} \) pixel value using \( j^{th} \) pixel will be as shown in Figure 2.

### RESULTS AND DISCUSSION

The original MR-Images are de-noised using modified NLM and NLM filter and the de-noised images are as shown in Figure 3.
For quantitative assessment, we have used different quality metrics such as MSE, PSNR, SSIM and PFOM. The graph of MSE, PSNR, SSIM, PFOM can be seen in Figure 4 to 8. We have calculated MSE, PSNR, SSIM and PFOM for 50 different MRI images and plotted the calculated values w.r.t. the image. Device Utilization Summary (estimated value) of Spartan 6 is as shown in Table 1.

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**Figure 3. Original and Denoised Image Using NLM**

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**Figure 4. Calculation of MSE for 50 different images**

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**Figure 5. Calculation of PSNR for 50 different images**
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Figure 6. Calculation of SSIM for 50 different images

Figure 7. Calculation of PFOM for 50 different images

Figure 8. Processing Time on Matlab and Xilinx for 10 different images

Table 1. Device Utilization of Spartan 6

| Device Utilization Summary (estimated value) | Logic Utilization | Utilization |
|---------------------------------------------|-------------------|-------------|
| Number of Slice Registers                   | 46                | 11440       | 0%          |
| Number of Slice LUTs                        | 76                | 5720        | 1%          |
| Number of Fully used LUT-FF pairs           | 41                | 81          | 50%         |
| Number of bonded IOBs                       | 13                | 200         | 6%          |
| Number of DSP48A1s                          | 1                 | 16          | 6%          |
From the graph of MSE, PSNR, SSIM, PFOM, we can observe that we are getting all these values near to ideal. Ideal value of SSIM has to be 1 and observed values are in the range 0.94 to 0.96 which shows very much similarity between original and denoised image. Also PFOM ideal value is 100% and the value that we have received is in the range 93% to 96%. Processing time of NLM using Xilinx is very less compared to Matlab implementation.

4. CONCLUSION

Based on the objective quality metrics, we can conclude that filter is effectively removing noise from the MRI. We can also show that the denoised image is good in terms of structure and edge profile from SSIM and PFOM. Also SSIM and PFOM show almost 95% matching with the original image. Also the time needed to denoise the complete image is very less compared to its matlab implementation. Algorithm implemented shows average 7000 times faster than the software implementation. So result demonstrate the advantage of implementation of NLM using FPGA compared to Matlab, hence can be considered as useful for MRI post processing.

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