Highly Sensitive and Selective Copper (II)-Catalyzed Dual-DNAzyme Colorimetric Biosensor Based on Exonuclease III-Mediated Cyclical Assembly

Baiqiang Zhai 1,2, Kunlun Huang 2, Hongtao Wang 1, Dongmin Su 1,3,* and Yuancong Xu 2,4,*

1 Henan Railway Food Safety Management Engineering Technology Research Center, Zhengzhou Railway Vocational & Technology College, Zhengzhou 451460, China; zhaibaiqiang@zzrvtc.edu.cn (B.Z.); 10554@zzrvtc.edu.cn (H.W.)
2 Beijing Laboratory for Food Quality and Safety, College of Food Science and Nutritional Engineering, China Agricultural University, Beijing 100083, China; hkl009@163.com
3 College of Food and Bioengineering, Zhengzhou University of Light Industry, Zhengzhou 450002, China
4 Beijing Key Laboratory of Environmental and Viral Oncology, Faculty of Environment and Life, Beijing University of Technology, Beijing 100124, China
* Correspondence: dongminsu@haut.edu.cn (D.S.); xuyuancong@bjut.edu.cn (Y.X.); Tel.: +86-0371-86608028 (D.S.); +86-010-67396139 (Y.X.)

Abstract: “Cu-DNAzyme” and “G4-DNAzyme” were used to develop a “turn-off” dual-DNAzyme colorimetric biosensor, which could be used to detect Cu^{2+} by employing exonuclease III-mediated cyclical assembly (EMCA). EMCA was based on the cleavage activity of Cu^{2+} to transfer the linkage sequences of the substrate strand and enzyme strand into the transition sequence. The horseradish peroxidase (HRP)-mimicking activity of the G4-DNAzyme was lost after binding with the complementary transition sequence and was hydrolyzed by Exo III. These results demonstrate that the proposed colorimetric biosensor was an effective method for ultradetection of trace metals in a high original signal background. Due to the high sensitivity of the biosensor, the limit of detection (LOD) of Cu^{2+} is 0.16 nM. This design offers a general purpose platform that could be applied for the detection of any metal ion target through adjustment of metal-dependent DNA-cleaving DNAzymes, which is of great significance for the rapid determination of food safety.

Keywords: copper ions; dual DNAzyme; exonuclease III-mediated cyclical assembly; biosensor

1. Introduction
Copper (Cu) is one of the most abundant trace elements in living organisms and is a common metal worldwide, and is widely utilized in agricultural and industrial fields [1]. Although copper is an important element, excessive intake could contribute to Parkinson’s, Wilson’s, and Alzheimer’s diseases and anemia [2]. The World Health Organization (WHO) and the European Union (EU) have recommended the highest copper concentration as 2 mg/L in human drinking water, while the U.S. Environmental Protection Agency (EPA) and the Ministry of Health in China have recommended the highest copper concentration as 1 mg/L in human drinking water.

The accurate measurement of Cu^{2+} with high selectivity and sensitivity is an important problem and has attracted increasing attention in recent years. Traditional analytical techniques for sensing Cu^{2+} depend upon expensive analytical equipment [3,4], but the on-site rapid detection of these methods is limited due to their complex sample pretreatments and high operating cost. Recently, biosensor methods that have shown good sensitivity and selectivity have been widely used in the rapid detection of Cu^{2+}, such as fluorescent biosensors [5,6], plasmonic biosensors [7,8], colorimetric biosensors [9,10], and electrochemical biosensors [11–13]. By comparing the aforementioned biosensors, Cu^{2+}-cleaving DNAzyme (Cu-DNAzyme) is the signal recognition and transition of choice, nucleic acid
amplification is the best method to increase sensitivity, and colorimetric analysis is the most convenient option.

Single-stranded DNA can bind to specific target molecules and exhibit catalytic activities, performing similarly to nucleic acid enzymes and protein enzymes under sequence-dependent tertiary structures [14]. Nucleic acid enzymes, including ribozymes (catalytic RNA) and deoxyribozymes (catalytic DNA or DNAzymes), can effectively catalyze RNA or DNA cleavage and have been frequently applied in sensing applications, such as Cu^{2+} [6,12,15], Pb^{2+} [16–18], Zn^{2+} [19,20], Mg^{2+} [21], UO_{2}^{2+} [22], and Cr^{3+} [23]. These methods render DNAzymes a terrific intermediary for sensing metal ions, and they have shown improved status compared with the normal direct detection method. The Cu-DNAzyme is formed from two DNA strands, which include substrate and enzyme. In the presence of Cu^{2+}, the substrate strand can be cleaved into two fragments, which can then be used in nucleic acid amplification. By combining cleavage and amplification, a high sensitivity method can be designed for the detection of Cu^{2+}.

Currently, nucleic acid amplification has been developed for the detection of metal ions in view of the transformation from metal ions to nucleic acids. Metal ion-mediated DNAzymes with cleavage activity are more suited for ssDNA amplification, such as strand displacement amplification (SDA) [18,19,24], rolling circle amplification (RCA) [25,26], and hybridization chain reaction (HCR) [20,23]. All of these methods are DNA replication isothermal technologies that have traditionally used specific primer sequences to generate multiple copies of a sequence library by DNA polymerase. However, there are some disadvantages with respect to template processing, primer design, reaction optimization, enzyme dependence, and sensitivity improvement. Considering the special structure of the Cu-DNAzyme, two DNA strands can be merged into one strand without disrupting its cleavage activity. Then, the combination of new Cu-DNAzyme and exonuclease (Exo) III strategies [27] can resolve the above problems. This paper proposes the concept of cyclic “hybridization–hydrolyzation” in order to achieve the detection of Cu^{2+}. Particularly for trace detection, which still faces challenges, our concept is able to meet this demand.

Cu-biosensors can also be classified, according to the characteristics of the signals, into turn-on [28] and turn-off [29] biosensors. For the turn-on biosensor, the signal intensity increases with increasing amounts of the target. Due to its strong specificity but low sensitivity, it is not appropriate for trace detection. For the turn-off biosensor, the signal intensity decreases with increasing amounts of the target. It can still maintain stable detection for low concentration targets, becoming the preferred strategy for trace detection. Colorimetric biosensors have the advantages of being convenient, inexpensive, and visible and have been widely used in turn-off biosensors. One of the typical representatives of colorimetric elements is G-quadruplex DNAzymes (G4-DNAzymes) [30]. The G4-DNAzymes exhibit superior peroxidase-like activity in the presence of hemin and are able to catalyze H_{2}O_{2}-mediated oxidation of 2,2′-azino-bis-(3-ethylbenzthiazoline-6-sulphonate) (ABTS), producing a green product (free-radical cation ABTS•^{+}) with a maximal absorption signal at a wavelength of ~419 nm. The integration of Cu-DNAzyme and G4-DNAzyme will further simplify the detection of Cu^{2+}. It also combines the advantages of specificity for signal recognition and sensitivity for signal visibility analysis.

In this paper, a highly sensitive “turn-off” dual DNAzyme colorimetric biosensor based on exonuclease III-mediated cyclical assembly (EMCA) for selecting and quantifying Cu^{2+} was developed. The principle of the proposed biosensor is depicted in Figure 1. As shown in Figure 1A, CUzyme comprises three parts: substrate strand (blue), linker sequence (red), and enzyme strand (green). The orange site in the substrate strand was the cleavage site. In the presence of Cu^{2+}, CUzyme was activated to irreversibly cleave the substrate strand at the cleavage site, producing two kinds of products. Due to its less stable intermolecular duplex structure, the cleaved substrate strands (blue, called the waste product) were released. For the remainder of CUzyme (called the first product), the spatial structure caused changes, forming a structured enzyme/linker complex with
a single strand tail, which would continue to participate in the subsequent reaction. The red tail is a complementary sequence of part of the G4-DNAzyme.

![Figure 1. Principles of the “turn-off” dual-DNAzyme colorimetric biosensor for Cu²⁺ ions. (A) Recognition of Cu²⁺; (B) EMCA; (C) color reaction.](image)

The details of the EMCA are shown in Figure 1B. The red tail could effectively hybridize with the G4-DNAzyme, forming a double strand complex with a blunt end. Then, the 3'-termini of G4-DNAzymes in the complex are hydrolyzed by Exo III, and this stimulates the release of the first product, the residual G4-DNAzyme (called the second product), and free bases (called the third product). The first product can further hybridize repeatedly with a new G4-DNAzyme, generating a cycle of hybridization–hydrolyzation. Due to the repeat “AGGG” in the G4-DNAzyme, the second product could further hybridize with the first product. Then, the introduction of the recessed 3'-termini could still trigger a hydrolyzation reaction by Exo III and the subsequent production of the abundant third product. The color reaction of the “turn-off” dual DNAzyme colorimetric biosensor is shown in Figure 1C. The G4-DNAzyme folds into many G-quadruplex structures that could combine with hemin to form an HRP-like DNAzyme, resulting in an increase in the absorbance signal due to an increased amount of green-colored ABTS⁺⁺. However, when Cu²⁺ ions are added to the complex, the G4-DNAzyme is hydrolyzed to a free base by Exo III. As a result, the biosensor has no absorbance signal and is colorless.

In summary, this report describes the construction of a “turn-off” dual DNAzyme colorimetric biosensor that combines the amplification features of EMCA with fluorescence detection by employing the G4-DNAzyme. This design offers a general purpose platform that could be applied for the detection of any other metal ion target through the adjustment of the metal ion-mediated DNAzyme, which is of great significance for the development of rapid detection technology in food safety.

2. Results
2.1. Feasibility of the Colorimetric Biosensor Based EMCA

This report describes the construction of a “turn-off” dual DNAzyme colorimetric biosensor that combines Cu-DNAzyme, EMCA, and G4-DNAzyme. The Cu-DNAzyme was employed as the recognition element of biosensor to achieve high specificity. EMCA amplification was developed to achieve signal reduction in biosensors. The G4-DNAzyme, as the detection element, is more applicable to the visual analysis of biosensor. As a result,
the success of our colorimetric biosensor was based on three dimensions: effective cleavage by Cu²⁺, effective hydrolysis by Exo III, and color reaction of G4-DNAzyme.

EMCA is driven by a free single strand tail. However, the tail could not be released unless Cu-DNAzyme was cleaved by Cu²⁺. Thus, the ability and efficiency of cleavage is one of the most important factors of the biosensor. In order to certify cutting efficiency, the experiments were carried out at different times. The length of the carboxyfluorescein (FAM)-labeled substrate (FAM-Cu-S) was 23 nt. In the presence of Cu²⁺, FAM-Cu-S was cleaved to 17 nt. As shown in Figure 2A, with increasing treatment time, the 23 nt and 17 nt bands gradually became shallow and dark, respectively. These results indicated that cutting efficiency increased with time and reached a peak after 10 min. Based on the brightness of Lane 1, the cleavage rate was quantified by Image Lab 4.1 software. As shown in Figure 2B, the cleavage rate was above 50% after cutting for 2 min and above 80% after cutting for 10 min. Considering the timeliness of the overall reaction, 5 min was selected as the final cutting time.

Figure 2. Cleavage rate of Cu²⁺ at different reaction times. (A) The results of dPAGE. Lanes 1–10: 0, 10 s, 30 s, 1 min, 2 min, 5 min, 10 min, 15 min, 30 min, and 60 min. (B) Cleavage rate.

EMCA was designed to breakdown the G4-DNAzyme. Moreover, the sustainability of EMCA was dependent on Exo III. Exo III displayed the ability to catalyze the stepwise digestion of mononucleotides from the recessed 3' terminus or the blunt part of the double-stranded DNA in order to recycle the target. Since signal reduction relied on Exo III, it was important to verify the hydrolysis. Due to the special G-quadruplex structure of the G4-DNAzyme, the complementary strand was used to verify the hydrolyzation reaction. Based on EMCA, G4-C and G4-M were designed to simulate the hybridization of the first product and the G4-DNAzyme. When FAM-labeled G4-C and G4-M meet, they bind to each other and form double-stranded DNA. Under the hydrolyzation reaction, Exo III could catalyze the removal of nucleotides from FAM-labeled G4-C in the 3' to 5' direction. As shown in Figure S1, a significant band in Lane 1 could be observed in the presence of FAM-labeled G4-C, and ladder bands were observed in Lane 2, indicating that FAM-labeled G4-C was degraded and generated different lengths of ssDNA. This phenomenon displayed a straightforward conclusion that G4-DNAzyme could also be degraded during EMCA, which inhibited color reactions.

Green signal of biosensor came from ABTS**, which was produced by the oxidation of ABTS with G4-DNAzyme. G4-DNAzyme is a G-rich sequence that has four continuous “GGG”, forming a stable G-quadruplex structure. Moreover, G4-DNAzyme was hydrolyzed by Exo III to different lengths of fragment. False-positive results might be caused if the fragment remained the HRP-mimicking activity. In order to avoid false-positives of the second product, the color reaction was tested by different lengths of G4-DNAzymes. G4-1 and G4-2 were designed by removing one and two “GGG”, respectively. G4-T-1 and G4-T-2 were designed to block one and two “GGG” in G4-DNAzyme, respectively. As shown in Figure S2, absorbance experiments under several conditions were carried out to demonstrate the feasibility of the biosensor. An intact G4-DNAzyme had a strong absorbance intensity and green color in the reaction. The absorbance intensity decreased in G4-1, which means that the deletion of “GGG” might not have a devastating impact on the G-quadruplex structure. However, G4-2 had no absorbance intensity, which means that G4-2 had no HRP-mimicking activity. When the G4-DNAzyme hybridizes with G4-T-1 or G4-T-2, the absorbance intensity can always be observed. This phenomenon explained
why the HRP-mimicking activity of G4-DNAzyme would not be totally blocked by the complementary strand. These two results comprehensively demonstrated that Exo III was essential in EMCA.

2.2. Develop and Optimize the Condition of the Biosensor

By exploration, a “turn-off” dual DNAzyme colorimetric biosensor was developed for the detection of Cu^{2+} ions. Moreover, the typical biosensor was verified with and without Cu^{2+} ions. The negative control was the mixture of GUzyme, G4-DNAzyme, hemin system, and ABTS system. As shown in Figure 3A, very strong absorbance intensity and green color were obtained in the negative control. In the experimental group, the absorbance intensity was significantly decreased by the presence of Cu^{2+}. The result indicated that G4-DNAzyme was successfully degraded. In order to achieve optimal sensing performance, the best detection parameters of the biosensor were determined. The absorbance change \( \frac{A_{b_0}}{A_{b_1}} \) was used to evaluate the biosensor, where \( A_{b_0} \) and \( A_{b_1} \) were the absorbance intensities in the absence and presence of Cu^{2+}, respectively. First, the concentration ratio of CUzyme to G4-DNAzyme was optimized. Figure 3B shows the effect of the concentration ratio on the \( \frac{A_{b_0}}{A_{b_1}} \) value. With a fixed concentration of CUzyme, \( \frac{A_{b_0}}{A_{b_1}} \) increased with increasing G4-DNAzyme. This indicated that G4-DNAzyme was successfully degraded in EMCA, and the degree of extinction was increased. However, when the ratio was over 1:2, the degree of extinction gradually decreased. This was caused by the strong background and limited hydrolysis of large amounts of G4-DNAzyme. As a result, the optimal concentration ratio of the CUzyme to the G4-DNAzyme was 1:2. Then, the concentration of Exo III was optimized. As shown in Figure 3C, \( \frac{A_{b_0}}{A_{b_1}} \) increased gradually with increasing Exo III and then reached a maximum value at 4 U. This indicated that hydrolysis by Exo III reached the saturation point. As a result, the optimal concentration of Exo III was 4 U. Finally, the reaction time was also investigated. As shown in Figure 3D, \( \frac{A_{b_0}}{A_{b_1}} \) increased with increasing reaction time. When the reaction time was over 30 min, \( \frac{A_{b_0}}{A_{b_1}} \) increased slowly. We suspected that the 3′-terminus of most G4-DNAzymes and some second products might be degraded in 30 min. The second products of varying length would be further degraded later. However, the rate of hydrolysis was slow due to the restriction of hybridization between the first product and the shorter second product. As a result, the optimal reaction time was 30 min.

Figure 3. (A) Colorimetric biosensor detection with and without Cu^{2+} ions; optimization of the experimental conditions. (B) Ratio of CUzyme and G4-DNAzyme; (C) concentration of Exo III; (D) reaction time. The concentration of the Cu^{2+} is 300 nmol/L.
2.3. Sensitivity for the Biosensor

In order to evaluate the sensitivity of the established biosensor, a serial dilution of Cu\(^{2+}\) ranging from 0 to 300 nM was used as a template for the optimized biosensor assays. Moreover, absorbance was measured at 412 nm. As shown in the Figure 4A, absorbance intensity decreased quickly with an increasing Cu\(^{2+}\) ion concentration from 0 to 300 nM. This phenomenon reveals that the absorbance change was indeed due to the catalyzed cleavage activity of CUzyme. When the concentration was over 200 nM, the absorbance intensity basically had no variation. This result meant that almost all of the CUzyme could be cleaved, and almost all of the G4-DNAzyme could be hydrolyzed under high concentration conditions. The relationship between Ab\(_0\)-Ab\(_1\) and Cu\(^{2+}\) concentrations is shown in Figure 4B. A good linear relationship was obtained from 1 to 200 nM and is represented by Y = 0.003692 × X + 0.03380 \((R^2 = 0.9916)\), where Y is Ab\(_0\)-Ab\(_1\), and X is the concentration (nM). The LOD was calculated at 0.16 nM on the basis of the average signal of the blank minus three times the standard deviation of the lowest analytical concentration. The detection limit of this approach was comparable to or even superior to other DNAzyme methods and more sensitive than the other analytical techniques for Cu\(^{2+}\) (Table S2).

![Figure 4. Sensitivity of the biosensor in response to various concentrations of Cu\(^{2+}\). (A) Absorbance intensity at 412 nm; (B) the linear relationship between Ab\(_0\)-Ab\(_1\) and the concentration.](image)

2.4. Selectivity for the Biosensor

For practical samples, copper is often confused with other heavy metal ions, so a high specificity is necessary for a reliable assay. This biosensor was controlled by CUzyme, so it must have a high level of selectivity for Cu\(^{2+}\). In order to certify its high specificity, 10 other relevant metal ions (Fe\(^{3+}\), Fe\(^{2+}\), Zn\(^{2+}\), Mg\(^{2+}\), Pb\(^{2+}\), Hg\(^{2+}\), Ca\(^{2+}\), Mn\(^{2+}\), Ni\(^{2+}\), and K\(^+\)) were tested were tested in this biosensor. As shown in Figure 5, the absorbance value can reflect the specificity of the biosensor. With the exception of Cu\(^{2+}\), almost all metal ions induced little absorbance change, and selectivity was much higher. In summary, the absorbance signal reduction displayed high selectivity for Cu\(^{2+}\) ions with this biosensor.

![Figure 5. Specificity of the biosensor for different metal ions. The concentration of all of the metal ions is 300 nM. “ns”: There was no significant difference; “****”: There was significant difference, \(p\) value < 0.0001.](image)
2.5. Application of the Biosensor in Tap Water Samples

Six kinds of tap water were analyzed by ICP-MS to ensure that there was no Cu\(^{2+}\) in them. In order to apply the proposed strategy to the highly sensitive detection of Cu\(^{2+}\) in environmental, water, soil, and food samples in the future, recovery experiments of Cu\(^{2+}\) were carried out in tap water. The water sample was processed with different concentrations of Cu\(^{2+}\) ions (10 µM, 20 µM, 40 µM, 60 µM, 80 µM, and 100 µM). The water sample was measured using the proposed strategy and ICP-MS three times. The recovery rates were 94.6–106% and 93.5–104% for the biosensor and ICP-MS, respectively (Table 1). These experimental results demonstrated the feasibility, accuracy, and practicability of the “turn-off” dual DNAzyme colorimetric biosensor for qualitative analysis in practical samples with little interference.

| Sample | Addition (nM) | Biosensor (nM) | Recovery Rate (%) | ICP-MS (nM) | Recovery Rate (%) |
|--------|---------------|----------------|-------------------|-------------|-------------------|
| 1      | 10            | 10.3 ± 0.3     | 103 ± 3           | 9.9 ± 0.5   | 99 ± 5            |
| 2      | 20            | 20.2 ± 0.5     | 101 ± 2.5         | 19.4 ± 0.7  | 97 ± 3.5          |
| 3      | 40            | 39.2 ± 0.7     | 98 ± 1.8          | 38.8 ± 0.8  | 97 ± 2            |
| 4      | 60            | 58.4 ± 1.6     | 97.3 ± 2.7        | 60.4 ± 1.9  | 100.7 ± 3.2       |
| 5      | 80            | 78.9 ± 1.4     | 98.6 ± 1.8        | 80.7 ± 1.6  | 100.9 ± 2         |
| 6      | 100           | 99.0 ± 1.3     | 99 ± 1.3          | 101.2 ± 2.8 | 101.2 ± 2.8       |

3. Materials and Methods

3.1. Materials and Reagents

All of the DNA oligonucleotides used in our study were synthesized by Invitrogen (Life Technologies, Carlsbad, CA, USA) and are listed in Table S1. Exo III was purchased from New England Biolabs, Inc., Ipswich, MA, USA. ABTS; hemin; dimethylsulfoxide (DMSO); H\(_2\)O\(_2\); tris (hydroxymethyl) aminomethane (Tris); tetramethylethylenediamine (TEMED); ethylenediamine tetraacetic acid disodium salt (EDTA); 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid (HEPES); and the metal salts, including Cu(NO\(_3\))\(_2\), Fe(NO\(_3\))\(_3\), Fe(NO\(_3\))\(_2\), Zn(NO\(_3\))\(_2\), Pb(NO\(_3\))\(_2\), Hg(NO\(_3\))\(_2\), Ca(NO\(_3\))\(_2\), Mn(NO\(_3\))\(_2\), Ni(NO\(_3\))\(_2\), and KCl, were purchased from Sigma Chemical Company (St. Louis, MO, USA).

3.2. Cu-DNAzyme Activity Assays

In order to prepare the Cu-DNAzyme complexes, the respective enzyme (1.5 µM) and carboxyfluorescein (FAM)-labeled substrate (1 µM) were mixed in a buffer (50 mM HEPES, 1.5 M NaCl, 50 µM sodium ascorbate, pH 7.0) and annealed at 95 °C for 3 min followed by slowly cooling to room temperature. In a typical experiment, 1 µM annealed Cu-DNAzyme was mixed with 1 µM Cu\(^{2+}\) solution in a buffer in order to initiate a cleavage reaction (total 7 µL). At the designated time point, the reaction was quenched by 7 µL gel loading buffer (8 M urea). The products were analyzed by 15% denaturing polyacrylamide gel electrophoresis (dPAGE) and imaged by a Bio-Rad ChemiDoc MP imaging system. Then, the intensities of the bands were analyzed by Image Lab 4.1 software.

3.3. The Procedure of EMCA and Dual-DNAzyme Colorimetric Biosensor

A Cu\(^{2+}\)-dependent DNAzyme (named CUzyme) was designed to explore the feasibility of EMCA. CUzyme was heated to 95 °C for 3 min, followed by gradual cooling to room temperature. The experiments were performed with 0.8 µM CUzyme, 1.6 µM G4-DNAzyme, 4 U Exo III, 1 × NEBuffer 1 (10 mM Bis-Tris-Propane-HCl, 10 mM MgCl\(_2\), 1 mM DTT, pH 7.0), and 300 nM Cu\(^{2+}\) and incubated for 60 min at 37 °C. The subsequent reaction products were analyzed by a chromogenic reaction. The assays were performed with 10 µL EMCA products, 10 µL hemin (12 µM), and 80 µL enzyme buffer (10 mmol/L NaH\(_2\)PO\(_4\)/Na\(_2\)HPO\(_4\), 100 mmol/L KCl, 2 mmol/L MgCl\(_2\), 0.003% Triton X-100, pH 7.0); incubation at 37 °C for 20 min; and then the addition of 30 µL colorimetric buffer was included (1 mL citrate buffer (pH 4.0) mixed with 5 µL ABTS (45 mmol/L) and 1 µL
30% H₂O₂). Then, the solution was incubated at room temperature for 5 min, and the absorbance at 412 nm was measured by using a Thermo Scientific Varioskan Flash (Thermo Scientific, Waltham, MA, USA).

3.4. Application of the Biosensor in a Real Sample

Tap water was collected from 6 districts in Beijing, China. The water samples were gently mixed with different concentrations of Cu²⁺. Then, the samples could be tested directly following the procedures described above.

4. Conclusions

In summary, an EMCA-based “turn-off” dual DNAzyme colorimetric biosensor was developed with highly sensitivity and specificity for Cu²⁺. The proposed strategy combines the advantages of CUzyme, EMCA, and G4-DNAzyme. The CUzyme as a recognition element shows high specificity and cleavage efficiency against other metal ions. The EMCA includes two steps, namely, hybridization and hydrolyzation. First, the remaining CUzyme changes its spatial conformation and drives its assembly with G4-DNAzyme. Second, the assembly products are digested by Exo III to release CUzyme, further driving a new EMCA process. The framework of the signal output in the biosensor is constructed by using G4-DNAzyme, which can catalyze the oxidation of ABTS by H₂O₂. More sensitive absorbance signal extinction can be achieved through hydrolysis reactions to form a number of free bases. As a result, the signal identification of the CUzyme, the signal extinction of the EMCA, and the signal detection of G4-DNAzyme can provide this biosensor with high levels of selectivity and sensitivity. Moreover, by changing the specific cleavage DNAzymes for other metal ions, this proposed strategy can easily be extended in order conveniently detect many other metal ions and will have wide applications in environmental, water, soil, and food sample analysis.

Supplementary Materials: The following are available online at https://www.mdpi.com/article/10.3390/catal11111352/s1, Figure S1: Hydrolyzing reaction of Exo III, Figure S2: Color reaction. Table S1: Oligonucleotides used in this study, Table S2: Comparison among previously reported method for the detection of Cu²⁺.

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References

1. Festa, R.A.; Thiele, D.J. Copper: An essential metal in biology. *Curr. Biol.* 2011, 21, R877–R883. [CrossRef] [PubMed]
2. Cotruvo, J.J.A.; Aron, A.T.; Ramos-Torres, K.M.; Chang, C.J. Synthetic fluorescent probes for studying copper in biological systems. *Chem. Soc. Rev.* 2015, 44, 4400–4414. [CrossRef]
3. Säbel, C.E.; Neureuther, J.M.; Siemann, S. A spectrophotometric method for the determination of zinc, copper, and cobalt ions in metalloproteins using Zincon. *Anal. Biochem.* 2010, 397, 218–226. [CrossRef]
4. Chen, J.; Teo, K.C. Determination of cadmium, copper, lead and zinc in water samples by flame atomic absorption spectrometry after cloud point extraction. *Anal. Chim. Acta* 2001, 450, 215–222. [CrossRef]
5. Wang, Z.; Jia, N.; Zhou, X.; Han, J.; Bu, H. Cu(I)-Catalyzed Click Reaction-Triggered 3D DNA Walker for Constructing an “OFF–ON” Fluorescent Biosensor for Cu²⁺ Detection. *ACS Appl. Bio Mater.* 2021, 4, 3571–3578. [CrossRef]
6. Tian, J.; Du, Z.; Zhu, L.; Shao, X.; Li, X.; Xu, W. Fluorescent detection of Cu (II) ions based on DNAzymatic cascaded cyclic amplification. Microchim. Acta 2020, 187, 443. [CrossRef]

7. Stebunov, Y.V.; Yakubovsky, D.I.; Fedyanin, D.Y.; Arsenin, A.V.; Volkov, V.S. Superior Sensitivity of Copper-Based Plasmonic Biosensors. Langmuir 2018, 34, 4681–4687. [PubMed]

8. Safran, V.; Göktürk, I.; Derazshamshir, A.; Yılmaz, F.; Sağlam, N.; Denizli, A. Rapid sensing of Cu$^{2+}$ in water and biological samples by sensitive molecularly imprinted based plasmonic biosensor. Microchem. J. 2019, 148, 141–150. [CrossRef]

9. Korkmaz, N.; Hwang, C.; Kessler, K.K.; Silina, Y.E.; Müller, L.; Park, J. A novel copper (II) binding peptide for a colorimetric biosensor system design. Talanta 2021, 232, 122439. [CrossRef]

10. Aktara, M.N.; Das, S.; Nayim, S.; Sahoo, N.K.; Beg, M.; Jana, G.C.; Maji, A.; Jha, P.K.; Hossain, M. A sensorial colorimetric sensor for the "turn-off" detection of iron(iii), iron(ii), and copper(ii) ions. Anal. Methods 2019, 11, 6–11. [CrossRef]

11. Liu, K.; Chen, K.S.; Sen, D.; Yu, H.-Z. Ultrasonic detection of total copper with an electrochemical biosensor built on the in cis rolling circle amplification. J. Hazard. Mater. 2020, 391, 122800. [CrossRef]

12. Atapour, M.; Amoabediny, G.; Ahmadzade-Raji, M. Integrated optical and electrochemical detection of Cu$^{2+}$ using a sandwich amino acid–gold nanoparticle-based nano-biosensor consisting of a transparent-conductive platform. RSC Adv. 2019, 9, 8882–8893. [CrossRef]

13. Zhen, J.; Yang, C.; Ye, H.; Wu, J.; Chen, Y. A novel copper (II) binding peptide for a colorimetric biosensor system design. Talanta 2021, 232, 122439. [CrossRef]

14. Cuenoud, B.; Szostak, J.W. A DNA metalloenzyme with DNA ligase activity. Nature 1995, 375, 611–614. [CrossRef] [PubMed]

15. Dou, Z.; Zhang, W.; Du, Q.; Liu, G. An in-situ plasmonic spectroscopy based biosensor for detection of copper (II) ions highlighting analytical specifications. Sensor. Actuat. B Chem. 2021, 329, 129103. [CrossRef]

16. Song, X.; Wang, Y.; Liu, S.; Zhang, X.; Wang, J.; Yang, J.; Zhang, F.; Yu, J.; Huang, J. A triply amplified electrochemical lead(II) sensor by using a DNAzyme and via formation of a DNA-gold nanoparticle nanoarray induced by a catalytic hairpin assembly. Microchim. Acta 2019, 186, 559. [CrossRef]

17. Fu, L.; Lu, Q.; Liu, X.; Chen, X.; Wu, X.; Xie, S. Combining whispering gallery mode optofluidic microbubble resonator sensor with GR-5 DNAzyme for ultra-sensitive lead ion detection. Talanta 2020, 213, 120815. [CrossRef]

18. Li, W.; Yang, Y.; Chen, J.; Zhang, Q.; Wang, Y.; Wang, F.; Yu, C. Detection of lead(II) ions with a DNAzyme and isothermal strand displacement signal amplification. Biosens. Bioelectron. 2014, 53, 245–249. [CrossRef] [PubMed]

19. Li, S.; Zhu, L.; Li, G.; Du, Z.; Tian, J.; Luo, Y.; Huang, K.; Xu, W. A “turn-off” ultra-sensitive fluorescent quantitative biosensor driven by zinc ion DNAzyme. Sensor. Actuat. B Chem. 2019, 285, 173–178. [CrossRef]

20. Li, S.; Li, G.; Du, Z.; Zhu, L.; Tian, J.; Luo, Y.; Huang, K.; Xu, W. The ultra-sensitive visual biosensor based on thermostatic triple step functional nucleic acid cascade amplification for detecting Zn$^{2+}$. Food Chem. 2019, 290, 95–100. [CrossRef]

21. Zhao, X.-H.; Zhang, L.-Z.; Zhao, S.-Y.; Cui, X.-H.; Gong, L.; Zhao, R.; Yu, B.-F.; Xie, J. Silver-ion-mediated Mg$^{2+}$-dependent DNAzyme activity for amplified fluorescence detection of cysteine. Analyst 2019, 144, 1982–1987. [CrossRef]

22. Wang, X.; Zeng, R.; Chu, S.; Tang, W.; Lin, N.; Fu, J.; Yang, J.; Gao, B. A quencher-free DNAzyme beacon for fluorescently sensing uranyl ions via embedding 2-aminopurine. Biosens. Bioelectron. 2019, 135, 166–172. [CrossRef] [PubMed]

23. Zhu, L.; Miao, M.; Shao, X.; Yao, Y.; Yu, W. A Universal Electrochemical Biosensor Using Nick-HCR Nanostructure as Molecular Gate of Nanochannel for Detecting Chromium(III) Ions and MicroRNA. Anal. Chem. 2019, 91, 14992–14999. [CrossRef] [PubMed]

24. Chen, X.; Wang, X.; Lu, Z.; Luo, H.; Dong, L.; Ji, Z.; Xu, F.; Huo, D.; Hou, C. Ultra-sensitive detection of Pb$^{2+}$ based on DNAzymes coupling with multi-cycle strand displacement amplification (M-SDA) and nano-graphene oxide. Sens. Actuat. B Chem. 2020, 311, 127898. [CrossRef]

25. Tang, D.; Xia, B.; Tang, Y.; Zhang, J.; Zhou, Q. Metal-ion-induced DNAzyme on magnetic beads for detection of lead(II) by using rolling circle amplification, glucose oxidase, and readout of pH changes. Microchim. Acta 2019, 186, 318. [CrossRef] [PubMed]

26. Liu, J.; Hu, Q.; Qi, L.; Lin, J.-M.; Yu, L. Liquid crystal-based sensing platform for detection of Pb$^{2+}$ assisted by DNAzyme and rolling circle amplification. J. Hazard. Mater. 2020, 400, 123218. [CrossRef]

27. Zhou, F.; Li, B. Exonuclease III-Assisted Target Recycling Amplification Coupled with Liposome-Assisted Amplification: One-Step and Dual-Amplification Strategy for Highly Sensitive Fluorescence Detection of DNA. Anal. Chem. 2015, 87, 7156–7162. [CrossRef]

28. Bayindir, S.; Toprak, M. A novel pyrene-based selective colorimetric and ratiometric turn-on sensing for copper. Spectrochim. Acta. A 2019, 213, 6–11. [CrossRef]

29. Zhu, X.; Duan, Y.; Li, P.; Fan, H.; Han, T.; Huang, X. A highly selective and instantaneously responsive Schiff base fluorescent sensor for the "turn-off" detection of iron(iii), iron(ii), and copper(ii) ions. Anal. Methods 2019, 11, 642–647. [CrossRef]

30. Yang, H.; Zhou, Y.; Liu, J. G-quadruplex DNA for construction of biosensors. TrAC Trends Anal. Chem. 2020, 132, 116060. [CrossRef]