Abstract

Background: The meniscus is a complex tissue whose cell biology has only recently begun to be explored. Published models rely upon initial culture in the presence of added growth factors. The aim of this study was to test a three-dimensional (3D) collagen sponge microenvironment (without added growth factors) for its ability to provide a microenvironment supportive for meniscal cell extracellular matrix (ECM) production, and to test the responsiveness of cells cultured in this manner to transforming growth factor-β (TGF-β).

Methods: Experimental studies were approved prospectively by the authors’ Human Subjects Institutional Review Board. Human meniscal cells were isolated from surgical specimens, established in monolayer culture, seeded into a 3D scaffold, and cell morphology and extracellular matrix components (ECM) evaluated either under control condition or with addition of TGF-β. Outcome variables were evaluation of cultured cell morphology, quantitative measurement of total sulfated proteoglycan production, and immunohistochemical study of the ECM components chondroitin sulfate, keratan sulfate, and types I and II collagen.

Result and Conclusion: Meniscal cells attached well within the 3D microenvironment and expanded with culture time. The 3D microenvironment was permissive for production of chondroitin sulfate, types I and II collagen, and to a lesser degree keratan sulfate. This microenvironment was also permissive for growth factor responsiveness, as indicated by a significant increase in proteoglycan production when cells were exposed to TGF-β (2.48 μg/ml ± 1.00, mean ± S.D., vs control levels of 1.58 ± 0.79, p < 0.0001). Knowledge of how culture microenvironments influence meniscal cell ECM production is important; the collagen sponge culture methodology provides a useful in vitro tool for study of meniscal cell biology.
Background
The meniscus of the knee is a complex dense fibrous biologic structure with a design to provide both stability and a shock-absorber function. Collagenous components of the extracellular matrix (ECM) help provide tensile strength, and proteoglycan ECM components contribute to the shock absorber function. The meniscus contains both a vascularized outer portion and an inner, avascular region.

Appropriate function of the menisci are needed for normal knee biomechanical function. Aging and degeneration of the menisci result in tears being a common knee injury; 15% of all sports knee injuries involve the meniscus [1]. Initial meniscal injury causes patient pain and disability, and further meniscal damage and/or loss is associated with degenerative joint changes ultimately leading to osteoarthritis [2-4]. In spite of patient pain and major health care costs involved with meniscal damage, research on the biology of the meniscal cells and the potential for tissue engineering applications for the meniscus are relatively new fields of endeavor [5].

Arnoczky has summarized major issues related to meniscal repair using scaffolds and cells [6], noting that although some preliminary data had been done using meniscal fibrochondrocytes, fibroblasts, or synovial cells to produce a fibrocartilaginous tissue, additional studies were needed to characterize the cellular features and ECM produced. Several of the biologic considerations involved in creating a tissue engineered meniscus have also been described by Arnoczky [7], who has summarized several of the important cell carrier (or scaffold) features, including support of cell proliferation and ECM production, diffusion of nutrients, possible use as a carrier for cytokines, and biomechanical considerations. The latter has been addressed also by Setton et al [8]. Cell carrier materials should also degrade at a rate similar to the cell deposition rate of the ECM [9].

Tissue engineering approaches include the use of cells in specific cell carrier constructs or scaffolds which can provide specific cellular microenvironments directing desired cellular activities, including ECM production, cell proliferation and activation of cell signaling pathways [10,11], or allow delivery of bioactive molecules, proteins or drugs [12,13].

In the present study, we primarily focus upon use of a collagen sponge scaffold for 3D human meniscal cell culture. Rodkey has illustrated previous use of a bovine collagen meniscus scaffold implanted in the medial meniscus of the dog [7]. Our laboratory has also previously used such a construct in autologous disc cell implantation in a small rodent model and in other studies evaluating ECM deposition by human disc cells [14-16].

In this work, we have a primary interest in the ability of cultured human meniscus cells to attach and expand within this carrier, and to produce collagens and proteoglycans between and around these 3D cultured cells. Meniscal cell responsiveness to TGF-β was also investigated.

Results
Meniscal cells grew well from the initial explant culture and expanded well in monolayer culture. As shown in Figure 1, cells in early (non-confluent) stages had a fibroblast-like morphology in monolayer, with prominent long cell processes extending from the cells.

An initial series of experiments assessed the utility of the micromass culture method with human meniscal cells. Figure 2 shows that the resulting cell pellet contained abundant proteoglycans; proteoglycans are stained pink in this figure. However, these micromass cultures were delicate, technically difficult to feed and maintain, and resulted in small specimens which were challenging to examine with histologic methods. Therefore, we next investigated a collagen sponge 3D microenvironment for meniscal cell culture.

Figure 1
Low confluence human meniscus cells are spindle-shaped in monolayer culture. Note long processes which extend from the cells. (Hoffman modulation contrast image; bar = 10 μm).
Meniscal cells were studied from 11 subjects to investigate cell behavior, ECM formation and to quantify proteoglycan production in 3D collagen sponge culture. Specimens of meniscal cells in this 3D construct were easily fed, handled and processed for histologic examination. The study population contained 7 males and 4 females; 7 medial and 7 lateral meniscal cultures were assessed. Mean age for the medial meniscal cell surgical patients was 65.2 years ± 10.9 (7) (mean ± S.D. (n)), and for the lateral meniscal cell surgical patients 67.2 ± 6.5 (7). Mean meniscal grades did not differ between the lateral and medial groups (3.5 ± 0.7 (7) vs 3.4 ± 0.5 (7), respectively).

Proteoglycan production in 3D culture over 14 days was assessed with the DMB assay. Total proteoglycan values (μg/ml ECM digest) did not differ between the lateral and medial study populations (2.097 ± 0.214 (7) vs 2.369 ± 0.272 (7), respectively).

Meniscal cells attached well to the 3D sponge surface as shown in Figure 3A. ECM produced by cells filled cavities within the 3D sponge matrix and was present between and around cells (Figure 3B). Along the margin of the sponge, at the sponge-media interface, cells formed a boundary layer which often consisted of several layers of cells (Figure 3C).

We next examined the response of human meniscal cells in 3D sponge culture during exposure to 5 ng/ml TGF-β. This portion of our study utilized meniscal cells derived form 7 lateral and 8 medial menisci from 9 subjects (8 females, 1 male). Mean subject age was 64.6 years ± 8.5 (9). Cells were derived from three grade 3 menisci, and 12 grade 4 menisci. Results were analyzed in terms of quantitative assessment of total proteoglycan production by control vs TGF-β-treated cells, and by immunohistologic examination of ECM components.

Exposure to TGF-β significantly increased proteoglycan production by cells in 3D sponge culture. TGF-β-treated cells had a mean proteoglycan level of 2.48 ± 1.00 (15), (mean ± S.D. (n)), whereas the mean paired control level was 1.58 ± 0.79 (15), p < 0.0001. Cells cultured in the presence of TGF-β showed normal morphology and good proliferation (Figure 4A and 4B).

Immunohistochemical studies were performed to evaluate in vitro 3D production of selected major ECM components: keratan sulfate, chondroitin sulfate, and types I and II collagens. For keratan sulfate, localization was primarily cytoplasmic, with scant keratan present in the ECM (data not shown). In contrast, chondroitin sulfate was abun-
dant in ECM surrounding cells in both control and TGF-β-treated meniscal cells (Figure 5A and 5B). Abundant type I collagen was seen in ECM under control culture conditions (Figure 5C); type I production was also extensive in the ECM of TGF-β-treated meniscal cells (Figure 5D). Although control cultures produced substantial amounts of type II collagen (Figure 5E), ECM formed by TGF-β-treated cells appeared to have qualitatively greater amounts (Figure 5F).

**Discussion**

In this study we have shown that cells from even lower grades of menisci with greater degeneration can be established in culture, expanded and passaged, and studied in 3D culture microenvironments. It is interesting to note that meniscal cells derived from one of our study subjects with a grade 0 meniscus (i.e. a healthy meniscus) yielded a proteoglycan production value not different from the study population means for the lateral and medial cells (2.421 μg/ml compared to the lateral mean of 2.097 and medial mean of 2.369). We have also tested cells from a 12 year old child with an osteosarcoma, again with a meniscal grade 0; this individuals proteoglycan production level in 3D culture was also similar to the study means (2.758). Thus, although our study has the shortcoming of utilizing primarily more degenerated menisci with grades 3–5, we have a small body of evidence that the 3D collagen sponge methodology works well with meniscal cells from both health and degenerated menisci.

Although several other recent tissue culture studies that have utilized other 3D methodologies, several have features which make those methods more difficult to use in experimental studies. Adesida et al. utilized a micromass-like methodology, but this required that the culture be carried out with supplemented chondrogenic factors (insulin, transferrin, selenite, dexamethasone, TGF-β) [17,18]. Such media additives should be kept in mind when evaluating the resulting cell phenotype.

Other meniscal cell culture methodologies include the gelatin hydrogel system utilized by Ishida et al. [19] and polylactic acid scaffolds as utilized by Stewart et al. [20], Marsano et al. [21], and Kang et al. [22]. The polylactic carrier systems are complicated by the acidic microenvironment associated with their degradation, and long-lasting presence of macrophages/giant cells during this process [23]. Previous work by Verdonk et al. utilized a more traditional alginate culture methodology, but histologic illustrations showed little ECM surrounding cells [24].

Our study presents data on a relatively small patient population. It is important that future additional work address cells derived from both medial and lateral meniscal sites, and that studies measure proteoglycan production at additional time points which will expand our data from 7 days of culture in micromass and 14 days of culture in 3D collagen sponges.

Because of the clinical importance of meniscal tears and meniscal degeneration, we hope that culture methods such as those described here will be used in future studies of meniscal cell gene expression and tissue engineering applications.

**Conclusion**

The present findings on ECM production under control conditions by human meniscal cells provides an important advance over routine monolayer cell culture. The 3D microenvironment provides cues to the cells in a fashion that is more like the in vivo condition of cells. Our studies here utilized 20% fetal bovine serum to accelerate prolif-
eration and thus lessen the time cells were kept in monolayer culture prior to experimental use. Although micromass culture did show ECM production, this technique is extremely tedious and limited in analytical studies. The collagen sponge, in contrast, is easily manipulated, does not require use of specialized chondrogenic media to allow ECM production, provides ample room for meniscal cell expansion and ECM production, and is easily embedded for morphologic studies.

Methods

(i) Clinical Study Population
Experimental studies were approved prospectively by the authors’ Human Subjects Institutional Review Board. Meniscal specimens were obtained from osteoarthritis patients undergoing total joint replacement surgery and transported immediately to the laboratory from the surgical suite. All the meniscal specimens obtained from osteoarthritis patients displayed clear signs of severe fibrillation and tears (grades 3 and 4). One meniscal specimen with normal-appearance (grade 0) was used in this study from a patient undergoing meniscectomy due to injury caused by an auto accident. Menisci were scored according to the following scale: grade 0, normal; grade 1, minimal fibrillation; grade 2, moderate fibrillation but without tears; grade 3, severe fibrillation and the presence of incomplete tears; grade 4, severe fibrillation with complete tears or multiple incomplete tears.

(ii) Monolayer cell culture
Meniscal cells were isolated from surgical specimens as previously described for the intervertebral disc using explant techniques [25] and expanded in monolayer culture for experimental use. Cells were cultured in sterile Modified Essential Media with Earle’s salts (MEM; Gibco, Grand Island, NY) with L-glutamine 1% (v/v) (Irvine Scientific, Santa Ana, CA), nonessential amino acids 1% (v/v) (Irvine Scientific), penicillin-streptomycin 1% (Irvine Scientific) and fetal bovine serum 20% (Gibco). All cultures were grown at 37°C under conditions of 95% relative humidity and 5% CO₂. Cells were fed with fresh media 3 times a week.

(iii) Standardized Design for 3D Sponge Cell Culture Experiments
Cells were P2 or 3 when used in experiments. Sterile Gelfoam® (Pharmacia & Upjohn Co., Kalamazoo, MI) sponges, an absorbable gelatin sponge prepared from
purified porcine skins gelatin USP granules, were trimmed into 0.5 cm³ cubes. Following preliminary studies testing cell concentrations, the work reported here used cell suspensions containing an average of 100,000 cells in Minimal Essential Medium with 20% fetal bovine serum (MEM20); this concentration was injected into each sponge cube with a pipette. Replicate collagen sponges were placed on Costar Transwell Clear Inserts (Costar) in 24-well plates and soaked with 2 ml MEM20. Seeded constructs were placed in the incubator (37°C, 5% CO₂, 95% humidity) and fed with fresh media 3 times a week. The TGF-β studies were carried out on cells cultured in 3D for 14 days with or without the addition of 5 ng/ml TGF-β (Sigma, St. Louis, MO). At the end of the 14 day period, replicate specimens were assessed either with histology and immunohistochemistry or for quantitative analysis of proteoglycan content (see below).

(iv) Micromass 3D Culture
Meniscal cells were also grown in micromass culture using modifications of Tare et al [26] and Paulsen and Solursh [27]. 200,000 cells were used to form each micromass culture. Micromass cultures were fed as described above and terminated after 7 days of culture. Upon termination, the micromass cultures were carefully transferred to a microcentrifuge tube, spun, and embedded in 1% sea plaque agarose to facilitate subsequent specimen handling. Micromasses were fixed in 10% neutral buffered formalin for 1 hour, placed in 70% ethanol, and processed for paraffin embedding.

(v) Morphologic and Immunohistochemical Analyses
At termination of culture, specimens were fixed in 10% neutral buffered formalin (Allegiance, McGaw Park, IL) for one hour and then transferred to 70% ethyl alcohol (AAPER, Shelbyville, KY) and processed in paraffin using a Shandon Pathcentre Automated Tissue Processor (ThermoShandon, Pittsburgh, PA). Specimens were embedded in Paraplast Plus (ThermoShandon) paraffin and 4 μm serial sections were cut with a Leica (Nussloch, Germany) RM2025 microtome. Sections were mounted on Superfrost-Plus microscope slides (Allegiance) and stained with toluidine blue for routine study, or were utilized for immunohistochemistry.

Immunohistochemistry
Collagen sponges were bisected and the two halves embedded on edge. Specimens were embedded in Paraplast Plus paraffin (ThermoShandon), and 4 mm serial sections cut with a Leica (Nussloch, Germany) RM2025 microtome and mounted on Superfrost-Plus microscope slides (Allegiance). Immunohistochemical localization of types I and II collagen, chondroitin sulfate, decorin and keratan sulfate utilized antibodies used techniques described previously [15,25]. The following antibodies were used at the indicated concentrations: anti-types I and II collagen (Biodesign International, Kennebunk, ME), 20 μg/ml; anti-keratan sulfate (Seikagaku Corporation, Tokyo, Japan), 5 μg/ml; anti-chondroitin sulfate (ICN Biomedicals, Costa Mesa, CA), 20 μg/ml. Endogenous peroxidase was blocked using 3% H2O2 (Humco, Texarkana, TX). The secondary antibody was Dako LSAB2 biotinylated Link for HRP/AP for 10 minutes followed by peroxidase-conjugated streptavidin (Dako) for 10 minutes and DAB (Dako) for 5 minutes. Slides were counterstained with light green, dehydrated, cleared and mounted with resinous mounting media. Negative controls consisted of Rabbit IgG (Dako, Carpinteria, CA, for collagen I and II) or mouse IgG (Dako, Carpinteria, CA, for all other antibodies) used at the same concentration as each antibody.

(vi) Biochemical total glycosaminoglycan determination
The 1,9 dimethylmethylen blue (DMB) assay was utilized to assess S-GAG production with modifications of the previously described method [28]. The DMB (Aldrich, Milwaukee, WI) solution was prepared and stored at room temperature in an amber bottle. Collagen sponge constructs containing cells were rinsed 3 times in Hank’s Balanced Salt Solution, HBSS, (Gibco, Carlsbad, CA). Replicates were combined in 1.5 ml microcentrifuge tubes and collagenase type V (Sigma) in HBSS (Gibco) was added to produce a final concentration of 1.0 Units/ml. The microcentrifuge tubes were incubated at 37°C until the sponge was completely digested (15–30 minutes). Samples were assayed in duplicate by mixing 0.1 ml of sample with 1.25 ml DMB solution. For standards, 0 – 7.5 μg chondroitin sulfate (Sigma, St. Louis, MO) was added to 1.25 ml DMB solution. All tubes were incubated at room temperature in the dark for 30 minutes followed by centrifugation at room temperature for 15 minutes at 10,000 rpm. One ml of the supernatant was removed and the absorbency read at 595 nm using a Beckman DU 600 spectrophotometer (Fullerton, CA). Formate buffer, pH 3.1, was used as a blank. Sample concentrations were determined from the standard curve and results expressed as μg S-GAG/ml.

(vii) Statistical analysis
Statistical analysis utilized standard methods using SAS software (version 8.2; SAS Institute, Cary, NC). Methods used included paired t-tests and Pearson correlation statistics. A p-value of less than 0.05 was considered statistically significant.

Abbreviations
3D: three-dimensional; ECM: extracellular matrix; TGF-β: transforming growth factor-beta; v: volume; MEM: Minimal Essential Media; DMB: dimethylmethylen blue; GAG: glycosaminoglycan.
Authors’ contributions
HEG: preparation of manuscript, experimental design, interpretation; DM: interpretation and specimen procurement; YC and JAI: laboratory work; ENH: interpretation; VS: specimen procurement, interpretation; HJN, statistical analysis.

Acknowledgements
The authors thank Patrick Honeycutt, B.S. for assistance with specimen transfer, Natalia Zinchenko, B.S. for expert histologic assistance, and Gretchen Hoelscher, M.S. for assistance with cell culture.

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