MiME: Multilevel Medical Embedding of Electronic Health Records for Predictive Healthcare

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Abstract
Deep learning models exhibit state-of-the-art performance for many predictive healthcare tasks using electronic health records (EHR) data, but these models typically require training data volume that exceeds the capacity of most healthcare systems. External resources such as medical ontologies are used to bridge the data volume constraint, but this approach is often not directly applicable or useful because of inconsistencies with terminology. To solve the data insufficiency challenge, we leverage the inherent multilevel structure of EHR data and, in particular, the encoded relationships among medical codes. We propose Multilevel Medical Embedding (MiME) which learns the multilevel embedding of EHR data while jointly performing auxiliary prediction tasks that rely on this inherent EHR structure without the need for external labels. We conducted two prediction tasks, heart failure prediction and sequential disease prediction, where MiME outperformed baseline methods in diverse evaluation settings. In particular, MiME consistently outperformed all baselines when predicting heart failure on datasets of different volumes, especially demonstrating the greatest performance improvement (15% relative gain in PR-AUC over the best baseline) on the smallest dataset, demonstrating its ability to effectively model the multilevel structure of EHR data.

1 Introduction
The rapid growth of electronic health record (EHR) data has motivated use of deep learning models and demonstrated state-of-the-art performance in diagnostics [26, 13, 12, 27], disease detection [14, 10, 17], risk prediction [20, 32], and patient subtyping [3, 6]. However, training optimal deep learning models typically requires a large volume (i.e. number of patient records and features per record) Most health systems do not have the data volume required to optimize performance of these models, especially for less common services (e.g. intensive care units (ICU)) or rare conditions.

External resources, particularly medical ontologies have been used to address data volume insufficiencies [12, 31, 7]. For example [12], latent embedding of a clinical code (e.g. diagnosis code) can be learned as a convex combination of the embeddings of the code itself and its ancestors on the ontology graph. However, medical ontologies are often not available or not directly applicable due to the nonstandard, or idiosyncratic use of terminology and complex terminology mapping from one health system’s EHR to another. For example, many clinics still use their own in-house terminologies.

Work done at Georgia Institute of Technology.
Work done at Sutter Health.
Figure 1: Symbolic representation of a single visit of a patient. Red denotes diagnosis codes, and blue denotes medication/procedure codes. A visit encompasses a set of codes, as well as a hierarchical structure and heterogeneous relations among these codes. For example, while both Acetaminophen and IV fluid form an explicit relationship with Fever, they also are correlated with each other as descendants of Fever.

for medications and lab tests, which do not conform with the standard medical ontologies such as Anatomical Therapeutic Chemical (ATC) Classification system and Logical Observation Identifiers Names and Codes (LOINC).

As an alternative, we explored how the inherent multilevel structure of EHR data could be leveraged to improve learning efficiency. The hierarchical structure of EHR data begins with the patient, followed by visits, then diagnosis codes within visits, which are then linked to treatment orders (e.g. medications, procedures). This hierarchical structure reveals influential multilevel relationships, especially between diagnosis codes and treatment codes. For example, a diagnosis fever can lead to associated treatments such as acetaminophen (medication) and IV fluid (procedure). We examine whether this multilevel structure could be leveraged to obtain a robust model under small data volume. To the best of our knowledge, none of the existing works leverage this multilevel structure in EHR. Rather, they flatten EHR data as a set of independent codes [18, 38, 11, 12, 14, 10, 13, 27, 2], which ignores hierarchical relationships among medical codes within visits.

We propose Multilevel Medical Embedding (MiME) to simultaneously transform the inherent multilevel structure of EHR data into multilevel embeddings, while jointly performing auxiliary prediction tasks that reflect this inherent structure without the need for external labels. Modeling the inherent structure among medical codes enables us to accurately capture the distinguishing patterns of different patient states. The auxiliary tasks inject the hierarchical knowledge of EHR data into the embedding process such that the main task can borrow prediction power from related auxiliary tasks. We conducted two prediction tasks, heart failure prediction and sequential disease prediction, where MiME outperformed baseline methods in diverse evaluation settings. In particular, for heart failure prediction on datasets of different volumes, MiME consistently outperformed all baseline models. Especially, MiME showed the greatest performance improvement (15% relative gain in PR-AUC over the best baseline) for the smallest dataset, demonstrating its ability to effectively model the multilevel structure of EHR data.

2 Method

EHR data can be represented by a common hierarchy that begins with individual patient records, where each patient record consists of a sequence of visits. In a typical visit, a physician gives a diagnosis to a patient and then order medications or procedures based on the diagnosis. This process generates a set of treatment (medication and procedure) codes and a relationship among diagnosis and treatment codes (see Figure 1). MiME is designed to explicitly capture the relationship between the diagnosis codes and the treatment codes within visits.

2.1 Notations of MiME

Assume a patient has a sequence of visits \( V^{(1)} \), \ldots, \( V^{(t)} \) over time, where each visit \( V^{(t)} \) contains a varying number of diagnosis (Dx) objects \( O_1^{(t)}, \ldots, O_{|V^{(t)}|}^{(t)} \). Each \( O_i^{(t)} \) consists of a single Dx code \( d_i^{(t)} \in A \) and a set of associated treatments (medications or procedures) \( M_i^{(t)} \). Similarly, each \( M_i^{(t)} \) consists of varying number of treatment codes \( m_{i,1}^{(t)}, \ldots, m_{i,|M_i^{(t)}|}^{(t)} \in B \). To reduce clutter, we omit
Table 1: Notations for MiME. Note that the dimension size \( z \) is used in many places due to the use of skip-connections, which will be described in section 2.2.

| Notation | Definition |
|----------|------------|
| \( \mathcal{A} \) | Set of unique diagnosis codes |
| \( \mathcal{B} \) | Set of unique treatment codes (medications and procedures) |
| \( \nu^{(t)} \) | A vector representation of a patient |
| \( v^{(t)} \in \mathbb{R}^z \) | A patient’s \( t \)-th visit, which contains diagnosis objects \( O_1^{(t)}, \ldots, O_{|\mathcal{V}|}^{(t)} \) |
| \( O_i^{(t)} \in \mathbb{R}^z \) | A vector representation of \( \nu^{(t)} \) |
| \( o_i^{(t)} \in \mathbb{R}^z \) | A vector representation of \( O_i^{(t)} \) |
| \( d_i^{(t)} \in \mathbb{R}^z \) | A vector representation of \( O_i^{(t)} \) |
| \( m_i^{(t)} \in \mathcal{B} \) | A vector representation of \( O_i^{(t)} \) |
| \( g(d_i^{(t)}, m_i^{(t)}) \) | Auxiliary predictions, respectively for a Dx code and a treatment code based on \( o_i^{(t)} \) |
| \( f(d_i^{(t)}, m_i^{(t)}) \) | A vector representation of \( O_i^{(t)} \) |
| \( r(\cdot) \in \mathbb{R}^z \) | A helper notation for extracting \( d_i^{(t)} \) or \( m_i^{(t)} \)'s embedding vector |

the superscript \((t)\) indicating \( t \)-th visit, when we are discussing a single visit. Table 1 summarizes notations we will use throughout the paper.

In Figure 1, there are five Dx codes, hence five Dx objects \( O_1^{(t)}, \ldots, O_5^{(t)} \). More specifically, the first Dx object \( O_1 \) has \( d_1^{(t)} = \text{Fatigue} \) as the Dx code, but no treatment codes. \( O_2 \), on the other hand, has Dx code \( d_2^{(t)} = \text{Cough} \) and two associated treatment codes \( m_1^{(t)} = \text{Benzonatate} \) and \( m_2^{(t)} = \text{Acetaminophen} \). In this case, we can use \( g(d_1^{(t)}, m_1^{(t)}) \) to capture the interaction between Dx code \( \text{Cough} \) and treatment code \( \text{Benzonatate} \), which will be fed to \( f(d_2^{(t)}, m_2^{(t)}) \) to obtain the vector representation of Dx object \( O_2^{(t)} \). Using the five Dx object embeddings \( o_1^{(t)}, \ldots, o_5^{(t)} \), we can obtain a visit embedding \( v^{(t)} \). In addition, some treatment codes (e.g. Acetaminophen) can be shared by two or more Dx codes (e.g. Cough, Fever), if the doctor ordered a single medication for more than one diagnosis. Then each Dx object will have its own copy of the treatment code attached to it, in this case denoted, \( m_2^{(t)} \) and \( m_3^{(t)} \), respectively.

### 2.2 Description of MiME

**Multilevel Embedding** As discussed earlier, previous approaches often flatten a single visit such that Dx codes and treatment codes are packed together so that a single visit \( \nu^{(t)} \) can be expressed as a binary vector \( x^{(t)} \in \{0, 1\}^{|\mathcal{A}|+|\mathcal{B}|} \) where each dimension corresponds to a specific Dx and treatment code. Then a patient’s visit sequence is encoded as:

\[
v^{(t)} = \sigma(W_x x^{(t)} + b_x) \quad h = h(v^{(1)}, v^{(2)}, \ldots, v^{(t)})
\]

where \( W_x \) is the embedding matrix that converts the binary vector \( x \) to a lower-dimensional visit representation \( x^{(t)} \) \( \sigma \) a non-linear activation function such as sigmoid or rectified linear unit (ReLU), \( h(\cdot) \) a function that maps a sequence of visit representations \( v^{(0)}, \ldots, v^{(t)} \) to a patient representation \( h(\cdot) \). In contrast, MiME effectively derives a visit representation \( v^{(t)} \), than can be plugged into any \( h(\cdot) \) for the downstream prediction task. \( h(\cdot) \) can simply be an RNN or a combination of RNNs and CNN and attention mechanisms.

MiME explicitly captures the hierarchy between Dx codes and treatment codes depicted in Figure 1. Figure 3 illustrates how MiME builds the representation of \( \nu \) (omitting the superscript \((t)\)) in a bottom-up fashion via multilevel embedding. In a single Dx object \( O_t \), a Dx code \( d_t \) and its associated treatment codes \( M_t \) are used to obtain a vector representation of \( O_t, o_t \). Then multiple Dx object embeddings \( o_0, \ldots, o_{|\mathcal{V}|} \) in a single visit are used to obtain a visit embedding \( v \), which in turn forms

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2 We omit bias variables throughout the paper to reduce clutter.
a patient embedding $h$ with other visit embeddings. The formulation of MiME is as follows:

$$v = \sigma \left( W_v \left( \sum_{i} f(d_i, \mathcal{M}_i) \right) \right) + F$$  \hspace{1cm} (1)

$$f(d_i, \mathcal{M}_i) = o_i = \sigma \left( W_o \left( r(d_i) + \sum_{j} g(d_i, m_{i,j}) \right) \right) + G$$  \hspace{1cm} (2)

$$g(d_i, m_{i,j}) = \sigma \left( W_m r(d_i) \right) \odot r(m_{i,j})$$  \hspace{1cm} (3)

where Eq. (1), Eq. (2) and Eq. (3) describe MiME in a top-down fashion, respectively corresponding to Visit level, Diagnosis level and Treatment level in Figure 2.

In Eq. (1), a visit embedding $v$ is obtained by summing Dx object embeddings $o_1, \ldots, o_{|V|}$, which are then transformed with $W_v \in \mathbb{R}^{2 \times z}$. $\sigma$ is a non-linear activation function such as sigmoid or rectified linear unit (ReLU). In Eq. (2), $o_i$ is obtained by summing $r(d_i) \in \mathbb{R}^z$, the vector representation of the Dx code $d_i$, and the effect of the interactions between $d_i$ and its associated treatments $\mathcal{M}_i$, which are then transformed with $W_o \in \mathbb{R}^{2 \times z}$. The interactions captured by $g(d_i, m_{i,j})$ are added to the $r(d_i)$, which can be interpreted as adjusting the diagnosis representation according to its associated treatments (medications and procedures). Note that in both Eq. (1) and Eq. (2), $F$ and $G$ are used to denote skip-connections [23].

In Eq. (3), the interaction between a Dx code embedding $r(d_i)$ and a treatment code embedding $r(m_{i,j})$ is captured by element-wise multiplication $\odot$. Weight matrix $W_m \in \mathbb{R}^{2 \times z}$ sends the Dx code embedding $r(d_i)$ into another latent space, where the interaction between $d_i$ and the corresponding $m_{i,j}$ can be effectively captured. The formulation of Eq. (3) was inspired by recent developments in bilinear pooling technique [37,21,19,24], which we discuss in more detail in Appendix A. With Eq. (3) in mind, $G$ in Eq. (2) can also be interpreted as $r(d_i)$ being skip-connected to the sum of interactions $g(d_i, m_{i,j})$.
Joint Training with Auxiliary Tasks Patient embedding $h$ is often used for specific prediction tasks, such as heart failure prediction or mortality. The representation power of $h$ comes from properly capturing each visit $V^{(t)}$, and modeling the longitudinal aspect with the function $h(V_0,...,V_t)$. Since the focus of this work is on modeling a single visit $V^{(t)}$, we perform auxiliary predictions as follows:

$$d_i^{(t)} = p(d_i^{(t)}|o_i^{(t)}) = \text{softmax}(U_d o_i^{(t)})$$  \hspace{1cm} (4)
$$m_{i,j}^{(t)} = p(m_{i,j}^{(t)}|o_i^{(t)}) = \sigma(U_m o_i^{(t)})$$  \hspace{1cm} (5)
$$L_{aux} = -\lambda_{aux} \sum_i \left( \sum_j \left( CE(d_i^{(t)}, \hat{d}_i^{(t)}) + \sum_j CE(m_{i,j}^{(t)}, \hat{m}_{i,j}^{(t)}) \right) \right)$$  \hspace{1cm} (6)

Given Dx object embeddings $o_1^{(t)},...,o_n^{(t)}$, while aggregating them to obtain $v^{(t)}$ as in Eq. 1, MiME predicts the Dx code $d_i^{(t)}$, and the associated treatment code $m_{i,j}^{(t)}$ as depicted by Figure 2. In Eq. 4 and Eq. 5, $U_d \in \mathbb{R}^{|A| \times z}$ and $U_m \in \mathbb{R}^{|B| \times z}$ are weight matrices used to compute the prediction of Dx code $\hat{d}_i^{(t)}$ and the prediction of the treatment code $\hat{m}_{i,j}^{(t)}$, respectively. In Eq. 6, $T$ denotes the total number of visits the patient made. $CE(\cdot,\cdot)$ the cross-entropy function and $\lambda_{aux}$ the coefficient for the auxiliary loss term. We used the softmax function for predicting $d_i^{(t)}$ since in a single Dx object $O_i^{(t)}$, there is only one Dx code involved. However, there could be no (or many) treatment codes associated with $O_i^{(t)}$, and therefore we used $|B|$ number of sigmoid functions for predicting each treatment code.

Auxiliary tasks are based on the inherent structure of the EHR data, and require no additional labeling effort. These auxiliary tasks guide the model to learn Dx object embeddings $o_i^{(t)}$ that are representative of the specific codes involved with it. Correctly capturing the events within a visit is the basis of all downstream prediction tasks, and these general-purpose auxiliary tasks, combined with the specific target task, encourage the model to learn visit embeddings $v^{(t)}$ that are not only tuned for the target prediction task, but also grounded in general-purpose foundational knowledge.

3 Experiments

In this section, we first describe the dataset and the baseline models, and present evaluation results. The source code of MiME is publicly available at \texttt{https://github.com/mp2893/mime}.

3.1 Source of Data

We conducted all our experiments using EHR data provided by Sutter Health. The dataset was constructed for a study designed to predict a future diagnosis of heart failure, and included EHR data from 30,764 senior patients 50 to 85 years of age. We extracted the diagnosis codes, medication codes and the procedure codes from encounter records, and related orders. We used Clinical Classification Software for ICD9-CM\footnote{https://www.hcup-us.ahrq.gov/toolssoftware/ccs/ccs.jsp} to group the ICD9 diagnosis codes into 388 categories. Generic Product Identifier Drug Group\footnote{http://www.wolterskluwercdi.com/drug-data/medi-span-electronic-drug-file/} was used to group the medication codes into 99 categories. Clinical Classifications Software for Services and Procedure\footnote{https://www.hcup-us.ahrq.gov/toolssoftware/ccs_svcsproc/ccssvcsproc.jsp} was used to group the CPT procedure codes into 1,824 categories. Any code that did not fit into the grouper formed its own category. Table 2 summarizes data statistics.

3.2 Baseline Models

First, we use Gated Recurrent Units (GRU)\footnote{https://www.hcup-us.ahrq.gov/toolssoftware/ccs/mc.jsp} with different embedding strategies to map visit embedding sequence $v^{(1)},...,v^{(T)}$ to a patient representation $h$:

- **raw**: A single visit $V^{(t)}$ is represented by a binary vector $x^{(t)} \in \{0,1\}^{|A|+|B|}$. Only the dimensions corresponding to the codes occurring in that visit is set to 1, and the rest are 0.
Table 2: Statistics of the dataset

|                           |        |
|---------------------------|--------|
| # of patients             | 30,764 |
| # of visits               | 616,073|
| Avg. # of visits per patient | 20.0   |
| # of unique codes         | 2,311  |
|                           | (Dx:388, Rx:99, Proc:1,824) |
| Avg. # of Dx per visit    | 1.93 (Max: 29) |
| Avg. # of Rx per diagnosis| 0.31 (Max: 17) |
| Avg. # of Proc. per diagnosis | 0.36 (Max: 10) |

- **linear**: The binary vector $x(t)$ is linearly transformed to a lower-dimensional vector $v(t) = W_x x(t)$ where $W_x \in \mathbb{R}^{b \times (|A|+|B|)}$ is the embedding matrix. This is equivalent to taking the vector representations of the codes (i.e. columns of the embedding matrix $W_x$) in the visit $V(t)$, and summing them up to derive a single vector $v(t) \in \mathbb{R}^{b}$.

- **sigmoid, tanh, relu**: The binary vector $x(t)$ is transformed to a lower-dimensional vector $v(t) = \sigma(W_x x(t))$ where we use either sigmoid, tanh, or ReLU for $\sigma(\cdot)$ to add non-linearity to linear.

- **sigmoid, mlp, tanh, mlp, relu, mlp**: We add one more layer to sigmoid, tanh and relu to increase their expressivity. The visit embedding is now $v(t) = \sigma(W_x, \sigma(W_x, x(t)))$ where $\sigma$ is either sigmoid, tanh or ReLU. We do not test linear, mlp since two consecutive linear layers can be collapsed to a single linear layer.

Second, we also compare with two advanced embedding methods that are specific designed for modeling EHR data.

- **Med2Vec**: We use Med2Vec [11] to learn visit representations, and use those fixed vectors as input to the prediction model. We test this model as a representative case of unsupervised embedding approach using EHR data.

- **GRAM**: We use GRAM [12], which is equivalent to injecting domain knowledge (ICD9 Dx code tree) to tanh via attention mechanism. We test this model as a representative case of incorporating external domain knowledge.

3.3 Prediction Tasks

**Heart failure prediction** The objective is to predict the first diagnosis of heart failure (HF), given an 18-months observation records discussed in section 3.1. Among 30,764 patients, 3,414 were case patients who were diagnosed with HF within a 1-year window after the 18-months observation. The remaining 27,350 patients were controls. The case-control selection criteria are detailed in [39] and summarized in Appendix B. While an accurate prediction of HF can save a large amount of costs and lives [33], this task is also suitable for assessing how well a model can learn the relationship between the external label (i.e. the label information is not inherent in the EHR data) and the features (i.e. codes).

We applied logistic regression to the patient representation $h$ to obtain a value between 0 (no HF onset) and 1 (HF onset). All models were trained end-to-end except Med2Vec. We report Area under the Precision-Recall Curve (PR-AUC) in the experiment and Area under the Receiver Operating Characteristic (ROC-AUC) in the appendix, as PR-AUC is considered a better measure for imbalanced data like ours [34,16]. Implementation and training configurations are described in Appendix C. We also performed sequential disease prediction (SDP) (predicting all diagnoses of the next visit at every timestep) where MiME demonstrated superior performance over all baseline models. The detailed description and results of SDP are provided in Appendix H and Appendix I respectively.

3.4 Experiment 1: Varying the Data Size

To evaluate MiME’s performance in another perspective, we created four datasets $E_1, E_2, E_3, E_4$ from the original data such that each dataset consisted of patients with varying maximum sequence length $T_{max}$ (i.e. maximum number of visits). In order to simulate a new hospital collecting patient records over time, we increased $T_{max}$ for each dataset such that 10, 20, 30, 150 for $E_1, E_2, E_3, E_4$ respectively. Each dataset had 6299 (414 cases), 15794 (1177 cases), 21128 (1848 cases), 27428 6
Figure 3: Test PR-AUC of HF prediction for increasing data size. A table with the results of all baseline models is provided in Appendix F.

(3173 cases) patients respectively. For \( \text{MiME aux} \), we used the same 0.015 for the auxiliary loss coefficient \( \lambda_{aux} \).

Figure 3 shows the test PR-AUC for HF prediction across all datasets (loss and ROC-AUC are described in Appendix G). Again we show the strongest activation functions \( \tanh \) and \( \tanh_{mlp} \) here and provide the full table in Appendix F. We can readily see that \( \text{MiME} \) outperforms all baseline models across all datasets. However, the performance gap between \( \text{MiME} \) and the baselines are larger in datasets \( E_1, E_2 \) than in datasets \( E_3, E_4 \), confirming our assumption that exploiting the inherent structure of EHR can alleviate the data insufficiency problem. Especially for the smallest dataset \( E_1 \), \( \text{MiME aux} \) (0.2831 PR-AUC) demonstrated significantly better performance than the best baseline \( \tanh_{mlp} \) (0.2462 PR-AUC), showing 15% relative improvement.

It is notable that \( \text{MiME} \) consistently outperformed \( \text{GRAM} \) in both Table 3 and Figure 3 in terms of test loss and test PR-AUC. To be fair, \( \text{GRAM} \) was only using Dx code hierarchy (thus ungrouped 5814 Dx codes were used), and no additional domain knowledge regarding treatment codes. However, the experiment results tell us that even without resorting to external domain knowledge, we can still gain improved predictive performance by carefully studying the EHR data and leveraging its inherent structure.

3.5 Experiment 2: Varying Visit Complexity

Table 3: HF prediction performance on small datasets. Values in the parentheses denote standard deviations from 5-fold random data splits. All models used GRU for mapping the visit embeddings \( v^{(1)}, \ldots, v^{(T)} \) to a patient representation \( h \). Two best values in each column are marked in bold. A full table with all baselines is provided in Appendix D.

|          | \( D_1 \) (Visit complexity 0-15%) | \( D_2 \) (Visit complexity 15-30%) | \( D_3 \) (Visit complexity 30-100%) |
|----------|-----------------------------------|-----------------------------------|-----------------------------------|
|          | (5608 patients, 464 cases)       | (5180 patients, 341 cases)       | (5231 patients, 383 cases)       |
| test loss| test PR-AUC | test loss | test PR-AUC | test loss | test PR-AUC | test loss | test PR-AUC |
| raw      | 0.2553 (0.0084) | 0.2669 (0.0314) | 0.2203 (0.0136) | 0.2388 (0.0460) | 0.2144 (0.0127) | 0.3776 (0.0580) |
| linear   | 0.2562 (0.0108) | 0.2722 (0.0354) | 0.2200 (0.0187) | 0.2403 (0.0229) | 0.2021 (0.0176) | 0.4339 (0.0411) |
| tanh     | 0.2648 (0.0124) | 0.2707 (0.0138) | 0.2186 (0.0182) | 0.2479 (0.0512) | 0.2025 (0.0151) | 0.4415 (0.0532) |
| tanh_{mlp} | 0.2587 (0.0121) | 0.2671 (0.0257) | 0.2289 (0.0213) | 0.2296 (0.0185) | 0.2024 (0.0181) | 0.4290 (0.0510) |
| Med2Vec  | 0.2601 (0.0166) | 0.2771 (0.0258) | 0.2171 (0.0170) | 0.2356 (0.0309) | 0.2044 (0.0129) | 0.3813 (0.0240) |
| GRAM     | 0.2554 (0.0254) | 0.2633 (0.0521) | 0.2249 (0.0448) | 0.2505 (0.0609) | 0.2333 (0.0362) | 0.3998 (0.0628) |
| \( \text{MiME} \) | 0.2535 (0.0042) | 0.2637 (0.0326) | 0.2121 (0.0238) | 0.2579 (0.0241) | 0.1931 (0.0140) | 0.4685 (0.0432) |
| \( \text{MiME aux} \) | 0.2512 (0.0073) | 0.2750 (0.0326) | 0.2117 (0.0238) | 0.2589 (0.0287) | 0.1910 (0.0163) | 0.4787 (0.0434) |

Next, we conducted a series of experiments to confirm that \( \text{MiME} \) can indeed capture the relationship between Dx codes and treatment codes, thus producing robust performance in small datasets. Specifically, we created three small datasets \( D_1, D_2, D_3 \) from the original data such that each dataset consisted of patients with varying degree of Dx-treatment interactions (i.e. visit complexity). We defined visit complexity as below to calculate for a patient the percentage of visits that have at least two diagnosis codes associated with different sets of treatment codes,

\[
\text{visit complexity} = \frac{\#V^{(t)} \text{ where } |\text{set}(\mathcal{M}_1^{(t)}, \ldots, \mathcal{M}_T^{(t)})| \geq 2}{T}
\]
where \( T \) denotes the total number of visits. For example, in Figure 1, the \( t \)-th visit \( V^{(t)} \) has Fever associated with no treatments, and Cough associated with two treatments. Therefore \( V^{(t)} \) qualifies as a complex visit. From the original dataset, we selected patients with a short sequence (less than 20 visits) to simulate a hospital newly equipped with a EHR system, and there aren’t much data collected yet. Among the patients with less than 20 visits, we used visit complexity ranges \( 0 – 15\%, 15 – 30\%, 30 – 100\% \) to create \( D_1, D_2, D_3 \) consisting of 5608 (464 HF cases), 5180 (341 HF cases), 5231 (383 HF cases) patients respectively. For training MiME with auxiliary tasks, we explored various \( \lambda_{aux} \) values between 0.01 – 0.1, and found 0.015 to provide the best performance, although other values also improved the performance in varying degrees.

Table 3 shows the HF prediction performance for the dataset \( D_1, D_2 \) and \( D_3 \). To enhance readability, we show here the results of the strongest activation function \( \text{tanh} \) and \( \text{tanh}_{mlp} \), and we report test loss and test PR-AUC. The results of other activation functions and the test ROC-AUC are provided in Appendix D and Appendix E.

Table 3 provides two important messages. First of all, both MiME and MiME \(_{aux} \) show close to the best performance in all datasets \( D_1, D_2 \) and \( D_3 \), especially high complexity dataset \( D_3 \). This confirms that MiME indeed draws its power from the interactions between Dx codes and treatment codes, with or without the auxiliary tasks. In \( D_1 \), patients’ visits do not have much structure, that it makes little difference whether we use MiME or not, and its performance is more or less similar to many baselines. Second, auxiliary tasks indeed help MiME generalize better to patients unseen during training. In all datasets \( D_1, D_2 \) and \( D_3 \), MiME \(_{aux} \) outperforms MiME in all measures, especially in \( D_3 \) where it shows PR-AUC 0.4787 (8.4\% relative improvement over the best baseline \( \text{tanh} \)).

4 Related Work

Over the years, medical concept embedding has been an active research area. Some works tried to summarize sparse and high-dimensional medical concepts into compressed vectors \([15, 18]\). In those works, medical concepts were organized as temporal sequences, from which embeddings were derived. Other works used latent layers of deep models for representing more abstract medical concepts \([14, 10, 13, 12, 27, 2] \). For example, restricted Boltzmann Machines, stacked auto-encoders or multi-layer neural networks were used to learn the representation of codes, visits, or patients \([38, 28, 11]\). Some works used medical ontologies to learn medical concept representations \([12, 8]\). Although all works successfully learned concept embeddings for some task in varying degrees, they did not fully utilize the multilevel structure or diagnosis-treatment relationship of EHR.

Recently, multiple code types in EHR gained more attentions. In \([35]\), authors viewed different code types separately, and tried to capture complex relationships across these disparate data types using RNNs, but they did not explicitly address the hierarchy of EHR data. More recently in \([30]\), the authors tried to explicitly capture the interaction between a set of all diagnosis codes and a set of all medication codes occurring in a visit. However, in their experiment, simply concatenating both sets to obtain a visit vector outperformed other methods in many tasks. This suggests that disregarding the diagnosis-specific Dx-Rx interaction and flattening all codes as sets is a suboptimal approach to modeling EHR data.

As described in section 2.2, we employ auxiliary task strategy to train a robust model. Training a model to predict multiple related targets has shown to improve model robustness in medical prediction tasks in previous studies. For example, \([5]\) used lab values as auxiliary targets to improve mortality prediction performance. More recent studies \([29, 22, 4]\) demonstrated improved prediction accuracy when training a model with multiple related tasks such as mortality prediction and phenotyping.

5 Conclusion

In this work, we presented MiME, an integrated approach that simultaneously models hierarchical inter-code relations into medical concept embedding while jointly performing auxiliary prediction tasks. Through extensive empirical evaluation, MiME demonstrated impressive performance across all benchmark tasks and its generalization ability to smaller datasets, especially outperforming baselines in terms of PR-AUC in heart failure prediction. As we have established in this work that MiME can be a good choice for modeling visits, in the future, we plan to extend MiME to include more fine-grained medical events such as procedure outcomes, demographic information, and medication instructions.
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Prevalence of heart failure signs and symptoms in a large primary care population identified through the use of text and data mining of the electronic health record. *Journal of Cardiac Failure*, 2014.
A Discussion of Bilinear Pooling

In Eq. (3), \( g(d_i, m_{ij}) \) uses a form of bilinear pooling to explicitly capture the interaction between the Dx code and the treatment code. The original bilinear pooling [37] derives a scalar feature \( f_i \) between two embeddings \( x, y \) such that \( f_i = x^T W_i y \) where \( W_i \) is a trainable weight matrix. Since we typically extract many features \( f_0, \ldots, f_i \), to capture the interaction between two embeddings, bilinear pooling requires us to train multiple weight matrices (i.e. weight tensor). Due to this requirement, researchers developed more efficient methods such as compact bilinear pooling [21, 19] and low-rank bilinear pooling [24], which is used in this work.

B Heart Failure Case-Control Selection Criteria

Case patients were 40 to 85 years of age at the time of HF diagnosis. HF diagnosis (HFDx) is defined as: 1) Qualifying ICD-9 codes for HF appeared in the encounter records or medication orders. Qualifying ICD-9 codes are displayed in Table 4. 2) a minimum of three clinical encounters with qualifying ICD-9 codes had to occur within 12 months of each other, where the date of diagnosis was assigned to the earliest of the three dates. If the time span between the first and second appearances of the HF diagnostic code was greater than 12 months, the date of the second encounter was used as the first qualifying encounter. The date at which HF diagnosis was given to the case is denoted as HFDx. Up to ten eligible controls (in terms of sex, age, location) were selected for each case, yielding an overall ratio of 9 controls per case. Each control was also assigned an index date, which is the HFDx of the matched case. Controls are selected such that they did not meet the operational criteria for HF diagnosis prior to the HFDx plus 182 days of their corresponding case. Control subjects were required to have their first office encounter within one year of the matching HF case patient’s first
Table 5: HF prediction performance of all models on small datasets. Values in the parentheses denote standard deviations from 5-fold random data splits. Two best values in each column are marked in bold.

| D1          | D2          | D3          |
|-------------|-------------|-------------|
| (Visit complexity 0-15%, 5688 patients) | (Visit complexity 15-30%, 5180 patients) | (Visit complexity 30-100%, 5231 patients) |
| test loss   | test loss   | test loss   |
| 0.2537 (0.0084) | 0.2691 (0.0314) | 0.2203 (0.0186) |
| linear      | linear      | linear      |
| 0.2562 (0.0108) | 0.2722 (0.0354) | 0.2209 (0.0187) |
| sigmoids    | sigmoids    | sigmoids    |
| 0.2594 (0.0062) | 0.2637 (0.0374) | 0.2198 (0.0200) |
| tanh        | tanh        | tanh        |
| 0.2648 (0.0124) | 0.2707 (0.0138) | 0.2186 (0.0182) |
| relu        | relu        | relu        |
| 0.2601 (0.0107) | 0.2546 (0.0109) | 0.2288 (0.0244) |
| sigmoidmlp  | sigmoidmlp  | sigmoidmlp  |
| 0.2836 (0.0102) | 0.1207 (0.0145) | 0.2407 (0.0162) |
| tanhmlp     | tanhmlp     | tanhmlp     |
| 0.2587 (0.0121) | 0.2671 (0.0257) | 0.2289 (0.0213) |
| relu64      | relu64      | relu64      |
| 0.2650 (0.0088) | 0.2643 (0.0148) | 0.2288 (0.0235) |
| Med2Vec     | Med2Vec     | Med2Vec     |
| 0.2601 (0.0186) | 0.2771 (0.0283) | 0.2171 (0.0170) |
| GRAM        | GRAM        | GRAM        |
| 0.2554 (0.0254) | 0.2633 (0.0521) | 0.2249 (0.0448) |
| MMiME       | MMiME       | MMiME       |
| 0.2535 (0.0042) | 0.2637 (0.0326) | 0.2121 (0.0238) |
| MMiMEmlp    | MMiMEmlp    | MMiMEmlp    |
| 0.2512 (0.0073) | 0.2750 (0.0326) | 0.2117 (0.0238) |

office visit, and have at least one office encounter 30 days before or any time after the case’s HF diagnosis date to ensure similar duration of observations among cases and controls.

C  Training Details

All models were implemented in TensorFlow 1.4 [36] and trained with a system equipped with Intel Xeon E5-2620, 512TB memories and 8 Nvidia Pascal Titan X’s. We used Adam [25] for optimization, with the learning rate $1e − 3$.

In all experiments, the reported results are averaged over 5-fold random data splits: training (70%), validation (10%) and test (20%). All models were trained with the minibatch of 20 patients for 20,000 iterations to guarantee convergence. At every 100 iterations, we evaluated the loss value of the validation set for early stopping.

For the non-linear activation functions in MMiME, we used ReLU in all places except for the one in Eq. (1) where we used sigmoid to benefit from its regularization effect. We avoid the vanishing gradient problem by using the skip connections. Note that simply adding skip connections to sigmoidmlp did not improve performance.

For the first experiment in section 3.5, size of the visit vector $v$ was 128 in all baseline models except raw. We ran a number of preliminary experiments with values 64, 128, 256 and 512, and we concluded that 128 was sufficient for all models to obtain optimal performance, as the datasets $D_1$, $D_2$ and $D_3$ were rather small. For MMiME, we adjusted the size of the embeddings $z$ to match the number of parameters to the baselines. Med2Vec was also trained to obtain 128 dimensional visit vectors. Note that sigmoidmlp, tanhmlp, relu64 and GRAM used 128 × 128 more parameters than other models. We used $L_2$ regularization with the coefficient $1e − 4$ for all models. We did not use any dropout technique. All models used GRU for the function $h(v^{(1)}, \ldots, v^{(T)})$ as described in section 3.3, the cell size of which was 128.

For the second experiment in section 3.4, where the models were trained on gradually larger datasets $E_1$, $E_2$, $E_3$ and $E_4$, the size of $v$ was set to 256 for all baseline models except raw. The same adjustments were made to MMiME as before, and the cell size of GRU was also set to 256.

D  Heart Failure Prediction Performance on Datasets $D_1$, $D_2$ and $D_3$, Full Version

Table 5 shows the performance of all models on datasets $D_1$, $D_2$ and $D_3$. An interesting finding is that both sigmoid and tanh mostly outperform relu in both measures in $D_1$, $D_2$ and $D_3$, although RelU is the preferred nonlinear activation for hidden layers in many studies. This seems due to the regularizing effect of sigmoid and tanh functions. Whereas RelU can produce outputs as high as infinity, sigmoid and tanh have bounded outputs. Considering that sigmoid, tanh and relu all sum up the code embeddings in a visit $v^{(i)}$ before applying the nonlinear activation, constraining the output of the nonlinear activation seems to work favorably, especially in $D_3$ where there are more
This regularization benefit, however, diminishes as the dataset grows, which can be confirmed by Table 7 in section F. In addition, as can be seen by the performance of sigmoid\_mlp, sigmoid clearly suffers from the vanishing gradient problem as opposed to tanh or ReLU that have larger gradient values.

### E ROC-AUC of Heart Failure Prediction on Datasets $D_1$, $D_2$ and $D_3$

Table 6: ROC-AUC of all models for HF prediction on small datasets. Values in the parentheses denote standard deviations from 5-fold random data splits. Two best values in each column are marked in bold.

| Model       | $D_1$ (Visit complexity 0-15%, 5608 patients) | $D_2$ (Visit complexity 15-30%, 5180 patients) | $D_3$ (Visit complexity 30-100%, 5231 patients) |
|-------------|---------------------------------------------|---------------------------------------------|---------------------------------------------|
| raw         | 0.7424 (0.0153)                             | 0.7508 (0.0254)                             | 0.8130 (0.0315)                             |
| linear      | 0.7298 (0.0187)                             | 0.7241 (0.0220)                             | 0.8209 (0.0130)                             |
| sigmoid     | 0.7220 (0.0098)                             | 0.7331 (0.0475)                             | 0.8200 (0.0128)                             |
| tanh        | 0.7273 (0.0050)                             | 0.7244 (0.0175)                             | 0.8171 (0.0151)                             |
| relu        | 0.7326 (0.0133)                             | 0.7078 (0.0181)                             | 0.8166 (0.0211)                             |
| sigmoid\_mlp| 0.5520 (0.0136)                             | 0.5770 (0.0416)                             | 0.7718 (0.0826)                             |
| tanh\_mlp   | 0.7215 (0.0188)                             | 0.7058 (0.0261)                             | 0.8080 (0.0258)                             |
| relu\_mlp   | 0.7205 (0.0122)                             | 0.7014 (0.0177)                             | 0.7993 (0.0212)                             |
| Med2Vec     | 0.7447 (0.0194)                             | 0.7515 (0.0243)                             | 0.8325 (0.0254)                             |
| GRAM        | 0.7586 (0.0240)                             | 0.6930 (0.0379)                             | 0.7785 (0.0260)                             |
| M1ME        | 0.7433 (0.0127)                             | 0.7723 (0.0232)                             | 0.8393 (0.0281)                             |
| M1ME\_aux   | 0.7449 (0.0117)                             | 0.7741 (0.0209)                             | 0.8435 (0.0244)                             |

Table 6 shows ROC-AUC of all models on datasets $D_1$, $D_2$ and $D_3$. Except for $D_1$ where patients have low visit complexity, M1ME again consistently outperforms all baseline models. However, the ROC-AUC gap between M1ME and baselines is not as great as PR-AUC. This is because ROC-AUC is determined by sensitivity (i.e. recall, or true positive rate) and specificity (i.e. true negative rate). A model achieves a high specificity if it can correctly identify as many negative samples as possible, which is easier for problems with many negative samples and few positive samples. PR-AUC, on the other hand, is determined by precision and recall. Therefore, for a model to achieve a high PR-AUC, it must correctly retrieve as many positive samples as possible while ignoring negative samples, which is harder for problems with few positive samples.

For heart failure (HF) prediction, achieving high specificity is relatively easy as there are way more controls (i.e. negative samples) than cases (i.e. positive samples). However, correctly identifying cases while ignoring controls requires a model to recognize what differentiates cases from controls. This means paying attention to the details of the patient records, such as the relationship between the diagnosis codes and treatment codes. That is why M1ME shows significant improvement in PR-AUC while showing moderate improvement in ROC-AUC. Also, this also explains why Med2Vec shows very poor PR-AUC as opposed to its competitive ROC-AUC. Med2Vec only pays attention to the co-occurrence of codes within a single visit, and not the interaction between diagnosis codes and treatment codes. It can work as a very efficient code grouper (codes that often appear in the same visit end up having similar code embeddings), leading to an increased ROC-AUC. But it cannot achieve a high PR-AUC, as that code grouping loses much of the subtle interaction between diagnosis codes and medication codes.

### F Test PR-AUC on Datasets $E_1$, $E_2$, $E_3$ and $E_4$, Full Version

Table 7 shows the PR-AUC of all models on datasets $E_1$, $E_2$, $E_3$ and $E_4$. It is notable that some baseline models show fluctuating performance as dataset grows. For example, tanh\_mlp showed competitive performance in small datasets, but weaker performance in large datasets. relu\_mlp, on the other hand, did not stand out in small datasets, but became the best baseline in large datasets. Such behaviors, along with the finding in Appendix D regarding the regularization effect, suggest that we should carefully choose activation functions of our model depending on the dataset size.

### G Test Loss and Test ROC-AUC on Datasets $E_1$, $E_2$, $E_3$ and $E_4$

Table 8 and Table 9 respectively shows the test loss and test ROC-AUC of all models on datasets of varying sizes $E_1$, $E_2$, $E_3$ and $E_4$. Both M1ME and M1ME\_aux consistently outperformed all baselines.
in terms of both test loss and test ROC-AUC, except Med2Vec. Moreover, M1M1 aux always showed better performance than M1M1 except test loss in E1, especially for the smallest dataset E1, confirming our assumption that auxiliary tasks can train a robust model when large datasets are unavailable. tanh_mlp consistently showed good performance in terms of ROC-AUC across all datasets, as opposed to showing fluctuating PR-AUC in Table 7. Med2Vec again showed a competitive ROC-AUC in all datasets, even outperforming M1M1 aux in E3. This suggests that initializing M1M1’s code embeddings with Med2Vec can be an interesting future direction as it may lead to an even better performance.

Table 8: Test loss of HF prediction for increasing data size. Parentheses denote standard deviations from 5-fold random data splits. Two best values in each column are marked bold.

|      | E1 (6299 patients) | E2 (15794 patients) | E3 (21128 patients) | E4 (27428 patients) |
|------|-------------------|---------------------|---------------------|---------------------|
| raw  | 0.2204 (0.0090)   | 0.2236 (0.0166)    | 0.2387 (0.0045)    | 0.2658 (0.0095)    |
| linear | 0.2299 (0.0078)  | 0.2345 (0.0160)    | 0.2395 (0.0068)    | 0.2642 (0.0099)    |
| sigmoid | 0.2229 (0.0064)  | 0.2215 (0.0135)    | 0.2373 (0.0034)    | 0.2655 (0.0095)    |
| tanh  | 0.2232 (0.0082)  | 0.2217 (0.0142)    | 0.2396 (0.0068)    | 0.2629 (0.0098)    |
| relu  | 0.2253 (0.0058)  | 0.2236 (0.0134)    | 0.2436 (0.0104)    | 0.2637 (0.0104)    |
| sigmoid_mlp | 0.2487 (0.0109) | 0.2681 (0.0140)  | 0.2964 (0.0054)    | 0.3335 (0.0063)    |
| tanh_mlp | 0.2198 (0.0058) | 0.2259 (0.0156)   | 0.2358 (0.0024)    | 0.2616 (0.0111)    |
| relu_mlp | 0.2175 (0.0067) | 0.2263 (0.0144)   | 0.2402 (0.0037)    | 0.2668 (0.0090)    |
| Med2Vec | 0.2162 (0.0091) | **0.2141 (0.0171)** | 0.2340 (0.0043)    | 0.2631 (0.0106)    |
| GRAM  | 0.2321 (0.0118)  | 0.2291 (0.0154)    | 0.2382 (0.0036)    | 0.2663 (0.0071)    |
| M1M1  | **0.2128 (0.0075)** | 0.2153 (0.0126) | **0.2331 (0.0039)** | **0.2559 (0.0096)** |
| M1M1 aux | **0.2111 (0.0089)** | **0.2122 (0.0115)** | **0.2326 (0.0048)** | **0.2557 (0.0095)** |

Table 9: Test ROC-AUC of HF prediction for increasing data size. Parentheses denote standard deviations from 5-fold random data splits. Two best values in each column are marked bold.

|      | E1 (6299 patients) | E2 (15794 patients) | E3 (21128 patients) | E4 (27428 patients) |
|------|-------------------|---------------------|---------------------|---------------------|
| raw  | 0.7585 (0.0202)   | 0.8083 (0.0265)    | 0.8165 (0.0146)    | 0.8330 (0.0111)    |
| linear | 0.7411 (0.0252)  | 0.7945 (0.0181)    | 0.8129 (0.0140)    | 0.8377 (0.0119)    |
| sigmoid | 0.7236 (0.0286)  | 0.7978 (0.0163)    | 0.8154 (0.0167)    | 0.8343 (0.0121)    |
| tanh  | 0.7419 (0.0247)  | 0.7943 (0.0186)    | 0.8121 (0.0146)    | 0.8388 (0.0117)    |
| relu  | 0.7366 (0.0267)  | 0.7891 (0.0197)    | 0.8105 (0.0210)    | 0.8353 (0.0123)    |
| sigmoid_mlp | 0.5191 (0.0269) | 0.5356 (0.0365)  | 0.6013 (0.0082)    | 0.6628 (0.0176)    |
| tanh_mlp | 0.7429 (0.0330) | 0.7796 (0.0283)   | 0.8172 (0.0084)    | 0.8431 (0.0128)    |
| relu_mlp | 0.7496 (0.0425) | 0.7837 (0.0217)   | 0.8047 (0.0131)    | 0.8331 (0.0100)    |
| Med2Vec | 0.7633 (0.0151) | **0.8141 (0.0213)** | **0.8301 (0.0138)** | **0.8445 (0.0115)** |
| GRAM  | 0.7575 (0.0218)  | 0.7828 (0.0228)    | 0.8077 (0.0107)    | 0.8313 (0.0083)    |
| M1M1  | **0.7676 (0.0292)** | 0.8109 (0.0223) | **0.8267 (0.0106)** | **0.8471 (0.0100)** |
| M1M1 aux | **0.7824 (0.0213)** | **0.8154 (0.0193)** | **0.8281 (0.0159)** | **0.8478 (0.0108)** |
Sequential Disease Prediction

In order to test if leveraging EHR’s inherent structure is a strategy generalizable beyond heart failure prediction, we test MiME’s prediction performance in another context, namely sequential disease prediction. The objective is to predict the diagnosis codes occurring in visit $V^{(t+1)}$ given all past visits $V^{(1)}, V^{(2)}, \ldots, V^{(t)}$. The input features are diagnosis codes $A$ and treatment codes $B$, while the output space only consists of diagnosis codes $A$. This task is useful for preemptively assessing the patient’s potential future risk [10], but is also appropriate for assessing how well a model captures the progression of the patient status over time. We used GRU as the mapping function $h(\cdot)$, and hidden vectors from all timesteps were fed to the softmax function with $|A|$ output classes to perform sequential prediction.

### Experiment Results for Sequential Disease Prediction

Table 10: Prediction performance for sequential disease prediction. Values in the parentheses denote standard deviations from 5-fold random data splits. The best value in each column is marked in bold.

|        | Test loss | Test recall@5 | Test recall@10 | Test recall@20 |
|--------|-----------|---------------|----------------|----------------|
| raw    | 7.2121 (0.0319) | 0.5329 (0.0016) | 0.6600 (0.0016) | 0.7749 (0.0019) |
| linear | 7.1474 (0.0321) | 0.5443 (0.0008) | 0.6749 (0.0010) | 0.7876 (0.0009) |
| sigmoid| 7.3494 (0.0438) | 0.5110 (0.0054) | 0.6338 (0.0052) | 0.7529 (0.0029) |
| tanh   | 7.1439 (0.0313) | 0.5456 (0.0016) | 0.6755 (0.0012) | 0.7879 (0.0010) |
| relu   | 7.1576 (0.0285) | 0.5427 (0.0011) | 0.6716 (0.0016) | 0.7846 (0.0015) |
| sigmoid_
mlp | 8.7886 (0.0257) | 0.2132 (0.0038) | 0.3466 (0.0031) | 0.5158 (0.0044) |
| tanh_
mlp | 7.1392 (0.0302) | 0.5470 (0.0010) | 0.6788 (0.0006) | 0.7926 (0.0009) |
| relu_
mlp | 7.1719 (0.0334) | 0.5433 (0.0010) | 0.6744 (0.0010) | 0.7876 (0.0012) |
| Med2Vec| 7.2429 (0.0283) | 0.5317 (0.0011) | 0.6583 (0.0020) | 0.7752 (0.0016) |
| GRAM   | 7.1738 (0.0361) | 0.5390 (0.0016) | 0.6685 (0.0025) | 0.7830 (0.0015) |
| MiME   | **7.1224 (0.0326)** | **0.5496 (0.0010)** | **0.6815 (0.0009)** | **0.7945 (0.0014)** |

After training all models until convergence, performance was measured by sorting the predicted diagnosis codes for $V^{(t+1)}$ by their prediction values, and calculating Recall@$k$ using the true diagnosis codes of $V^{(t+1)}$.

Table 10 shows the performance of all models for sequential disease prediction. MiME demonstrated the best performance in all metrics, showing that MiME can properly capture the temporal progression of the patient status. It is noteworthy that linear displayed very competitive performance compared to the best performing models. This is due to the fact that chronic conditions such as hypertension or diabetes persist over a long period of time, and sequentially predicting them becomes an easy task that does not require an expressive model. This was also reported in [10] where a strategy to choose the most frequent diagnosis code as the prediction showed competitive performance in a similar task.

In order to study whether explicitly incorporating the structure of EHR helps when there are small data volume, we calculated the test performance in terms of Precision@5 for predicting each diagnosis (Dx) code of $A$. In Table 11 we report average Precision@5 for four different groups of Dx codes, where the groups were formed by the rarity/frequency of the Dx codes in the training data. For example, the first column represents the Dx codes that appear in the 0.01%-0.05% of the entire visits (433407) in the training data, which are very rare diseases. On the other hand, the Dx codes in the last column appear in maximum 13.39% of the visits, indicating high-prevalence diseases. We selected the best performing activation function tanh among the three.

As can be seen from Table 11 except for the rarest Dx codes, MiME outperforms all other baseline models, as much as 11.6% relative gain over tanh_mlp. It is notable that Med2Vec demonstrated the greatest performance for the rarest Dx code group. However, the benefit of using pre-trained embedding vectors quickly diminishes to the point of degrading the performance when there are at least several hundred training samples.

Overall, MiME demonstrated good performance in prediction tasks in diverse settings, and it is notable that they significantly outperformed the baseline models in the more complex task, namely HF.
Table 11: Accuracy@5 for predicting diseases grouped by their rarity. The prevalence percentages are calculated by dividing the number of occurrences of each disease by 433407, the total number of visits in the training data. All values are averaged from 5-fold cross validation.

| Model     | 20th-40th percentile (0.01%-0.05% preval) | 40th-60th percentile (0.05%-0.2% preval) | 60th-80th percentile (0.2%-0.8% preval) | 80th-100th percentile (0.8%-13.4% preval) |
|-----------|------------------------------------------|------------------------------------------|------------------------------------------|------------------------------------------|
| raw       | 0.0530 (0.0156)                          | 0.1907 (0.0128)                          | 0.2999 (0.0039)                          | 0.4304 (0.0052)                          |
| linear    | 0.0633 (0.0203)                          | 0.2162 (0.0163)                          | 0.3266 (0.0053)                          | 0.4388 (0.0051)                          |
| tanh      | 0.0674 (0.0182)                          | 0.2101 (0.0143)                          | 0.3218 (0.0045)                          | 0.4379 (0.0033)                          |
| tanh_{mlp} | 0.0723 (0.0165)                         | 0.2353 (0.0118)                          | 0.3388 (0.0044)                          | 0.4381 (0.0034)                          |
| Med2Vec   | **0.1156** (0.0101)                      | 0.2240 (0.0155)                          | 0.3177 (0.0076)                          | 0.4217 (0.0046)                          |
| GRAM      | 0.0574 (0.0121)                          | 0.1634 (0.0057)                          | 0.3053 (0.0089)                          | 0.4409 (0.0039)                          |
| MIME      | 0.0965 (0.0154)                          | **0.2625** (0.0209)                      | **0.3597** (0.0082)                      | **0.4447** (0.0034)                      |

prediction, where the relationship between the label and the features (i.e. codes) from the data was more than straightforward.