Analytical Investigation of Peristaltic Transport of Power Law Fluid through a Tube

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Abstract
In this paper, the peristaltic flow of a power law fluid in a cylindrical channel is studied analytically. The governing equations consist of continuity and momentum equations are solved mathematically by perturbation method. The zeroth and first order in amplitude ratio of the stream function is considered for perturbation series. The effects of flow behavior index (n) flow rate and amplitude ratio (ε) on the flow field are investigated. The results show that increment of power law index predicts more flow rate and less pressure rise in peristaltic motion. Trapping phenomenon is form by closed stream line depending on peristaltic motion.

Keywords: Peristaltic motion; Power law fluid; Perturbation method; Cylindrical cannel

Introduction
Analysis of peristaltic flow has great practical importance in many biological and biomedical systems such as the flow of urine through the urethra, the swallowing process through the esophagus, the movement of spermatozoa in the ducts efferent of the male reproductive tract, transport of lymph in the lymphatic vessels and in the vasomotor of small blood vessels such as arterioles, venules and capillaries. Latham [1] was probably the first to investigate the mechanism of peristalsis in relation to mechanical pumping. Primary analytical studies of peristaltic transport for Newtonian fluids were performed by Shapiro et al. [2] in wave frame and by Fung and Yih [3] in laboratory frame. Peristaltic flow of a power-law fluid in a channel under long wavelength approximation was studied by Radhakrishnamacharya [4]. Srivastava and Srivastava [5] were investigated the peristaltic flow in blood vessels for the Casson fluid. Mernone and Mazumdar studied Casson fluid in Peristaltic motion by perturbation method [6]. The peristaltic transport of a power-law fluid in the male reproductive tract was studied by Srivastava and Srivastava [7]. Peristaltic pumping of two layered power-law fluids in cylindrical tube was investigated by Usha and Rao [8]. Eytan and Elad [9] and Eytan et al. [10] have studied the intra uterine fluid flow in the sagittal cross section of the uterus by an asymmetric channel under lubrication approach. The lubrication approach assumes that the width of the channel is very small compared with length. Mishra and Rao [11] have studied the peristaltic flow in asymmetric channels with asymmetry generated by different amplitudes of the peristaltic waves in addition to different phases. Takabatake and Ayukava [12] and Takabatake et al. [13] studied the problem of urine flow through a channel and a circular cylindrical tube, respectively by employing finite difference technique and discussed the phenomena of trapping and reflux. Siddiqui and Schwars studied on trapping for second-order fluid [14]. Recent investigations focused on numerical simulation of peristaltic flow in large variety of geometries [15-21].

In this paper, the peristaltic flow of a power law fluid in a cylindrical channel is investigated by using a perturbation method in the wave frame. The effects of main parameters of flow rate, Reynolds number, flow behavior index (n) and amplitude ratio (ε) on the flow regime are studied.

Governing equations
The physical model and related parameters are illustrated in the figure. The dimensionless parameters are defined as follows:

\[ \varepsilon = \frac{A}{d}, \quad \lambda = \frac{Z}{d}, \quad \lambda = \frac{R}{d}, \quad \lambda = \frac{G}{d}, \quad t = \frac{ct}{d} \]

\[ \alpha = \frac{2\pi d}{\lambda}, \quad \lambda = \frac{V_k}{c}, \quad \lambda = \frac{V_k}{c}, \quad \psi = \frac{\mu}{\rho d^2}, \quad \rho = \frac{\rho}{\rho d^2}, \quad Re = \frac{d^2 c_s^2 \rho}{m} \]

It is imagined that \( \alpha^2 \) is in the order of \( \varepsilon \) and the wave equation propagated along the tube is cosine form:

\[ G(Z, t) = d + A \cos \frac{2\pi d}{\lambda} (Z - ct) \] (1)

In the above equation \( d \) is the half non-deformed width of the channel, \( A \) is wave amplitude, \( \lambda \) is wave length, \( Z \) is longitudinal coordinate along the tube, \( c \) is wave velocity and \( t \) is time. Peristaltic motion is an unsteady phenomenon instinctively but it can be assumed steady if the coordinates travels with the velocity of wave so as it is shown in Figure 1, two fixed (laboratory frame) and moving (wave frame) coordinate can be defined in the following relation:

\[ z = z + ct, \quad r = r \]

(2)

Figure 1. The dimensionless parameters are defined as follows:

- **Figure 1**: Illustration of peristaltic motion.
\[ \mathbf{V}_Z = \mathbf{V}_z + c \quad \mathbf{V}_s = \mathbf{V}_s, \]  
(3)

Where \((\mathbf{V}_z, \mathbf{V}_s)\) and \((\mathbf{V}_s', \mathbf{V}_s')\) are the velocity component in the laboratory and wave frame for axial and radial direction respectively. Z-axis is the center line and R is the distance measured radial.

Governing equations consist of continuity and momentum equations in laboratory frame are in the following form:

**Continuity**

\[ \frac{\partial \rho}{\partial t} + \frac{1}{R} \frac{\partial (\rho v_z)}{\partial R} + \frac{1}{R} \frac{\partial (\rho v_s)}{\partial \theta} + \frac{\partial (\rho v_s)}{\partial Z} = 0 \]  
(4)

**R-Momentum**

\[ \rho \left( \frac{\partial v_z}{\partial t} + v_z \frac{\partial v_z}{\partial R} + v_s \frac{\partial v_s}{\partial R} + v_s \frac{\partial v_s}{\partial Z} \right) = \frac{\partial p}{\partial R} \left[ \frac{1}{R} \frac{\partial (R u_z)}{\partial R} \right] + \frac{1}{R} \frac{\partial (\rho v_s)}{\partial \theta} + \frac{\partial (\rho v_s)}{\partial Z} \]  
(5a)

**Z-Momentum**

\[ \rho \left( \frac{\partial v_s}{\partial t} + v_s \frac{\partial v_s}{\partial R} + v_s \frac{\partial v_s}{\partial \theta} + v_s \frac{\partial v_s}{\partial Z} \right) = \frac{\partial p}{\partial Z} \left[ \frac{1}{R} \frac{\partial (R u_s)}{\partial R} \right] + \frac{1}{R} \frac{\partial (\rho v_s)}{\partial \theta} + \frac{\partial (\rho v_s)}{\partial Z} \]  
(5b)

Also the boundary conditions are:

\[ \mathbf{V}_Z = 0, \quad \mathbf{V}_s = \frac{\partial \rho}{\partial t} G(Z,t) = -c \frac{\partial G}{\partial Z} @ R = G(Z,t) \]  
(6a)

\[ \mathbf{V}_s = 0, \quad \frac{\partial v_s}{\partial R} = 0 @ R = 0 \]  
(6b)

In the above equations for obtaining the stress term for power law fluid, (power law fluid is considered as a simple shear fluid) the constructive equation is defined as:

\[ \eta \left( U_{\sigma 22} \right) = m \eta \gamma \left( \gamma \right) \quad \\eta \gamma \left( \gamma \right) = m \eta \gamma \left( \gamma \right) \]  
(7)

Where \( U_{\sigma 22} \) is second invariant of strain rate tensor, \( n \) is flow behavior index, \( m \) is flow consistency and \( \gamma \) is defined as shear rate:

\[ \gamma = 2D \left[ \frac{\partial \mathbf{u}_2}{\partial \mathbf{X}_2} \right] \]  
(8)

Let \( u \) and \( v \) be the longitudinal \( v \) and transverse \( v \) velocity components respectively, the stress tensor will be:

\[ \tau = \begin{bmatrix} m \left( \frac{\partial v_z}{\partial R} \right)^2 & 0 & m \left( \frac{\partial v_z}{\partial R} + \frac{\partial v_s}{\partial R} \right)^2 \\ 0 & m \left( \frac{\partial v_s}{\partial \theta} \right)^2 & 0 \\ m \left( \frac{\partial v_s}{\partial Z} + \frac{\partial v_z}{\partial Z} \right)^2 & 0 & m \left( \frac{\partial v_s}{\partial Z} \right)^2 \end{bmatrix} \]  
(9)

By defining stream function for 2D flow and applying dimensionless parameters the non-dimensional governing equations and boundary conditions become as follows:

\[ \mathbf{V}_s = \frac{1}{R} \frac{\partial \psi}{\partial Z} \quad \mathbf{V}_z = \frac{1}{R} \frac{\partial \psi}{\partial R} \]  
(10)
\[ p = P, \quad \psi = \psi(R) \]

By substituting the stream function series in momentum equations for the zeroth-order momentum equations will be:

\[ \frac{\partial p}{\partial R} = 0 \]  

\[ \frac{\partial}{\partial R} \left( \frac{1}{Re} \frac{1}{R} \frac{1}{\psi^{(0)}} - \frac{1}{R} \frac{1}{\psi^{(1)}} \right) \]

(15)

(16)

\[ n \left( \frac{2}{R} \psi^{(0)} - \frac{2}{R} \psi^{(1)} \right) \left( \frac{1}{R} \frac{1}{\psi^{(0)}} - \frac{1}{R} \frac{1}{\psi^{(1)}} \right)^{-1} \]

(17)

The \( Z \)-momentum equations with the boundary conditions (13a, 13c) can be calculated analytically and \( \psi \), and \( \Delta P \) will be:

\[ \psi = B - \frac{n}{n+1} \left( \frac{1}{R} \frac{1}{\psi^{(0)}} + \frac{n}{3n+1} \right) \]

Where:

\[ B = \left( \frac{Re \delta P}{2 \epsilon Z} \right)^{1/3} \]

(18)

The flow rate is found by the following relation:

\[ q = \int_0^{2\pi/3} \int_0^{\delta} R \psi dR d\theta \]

(19)

As we had:

\[ - \frac{\partial \psi}{\partial R} \frac{1}{\psi^{(0)}} \]

(20)

So

\[ q = 2\pi \left( \psi^{(1)} + \epsilon \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) - \psi^{(0)} \right) \]

(21)

Taylor expansion results:

\[ q = 2\pi \left( \psi^{(1)} + \epsilon \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \psi^{(1)} \right) \]

(22)

It is important to find the flow over a period of time \( T \) at the fixed cross section position that is called time-mean flow as:

\[ \overline{Q} = \frac{1}{T} \int_0^T q d\tilde{t} \]

Where \( T \) is:

\[ T = \frac{\lambda}{c} \]

Finally:

\[ \overline{Q} = 2\pi \frac{T}{\lambda} \left( \frac{n}{2(3n+1)} \right) d\tilde{t} + 2\pi \frac{T}{\lambda} \epsilon \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) d\tilde{t} \]

(23)

(24)

Since the second part of right hand side of above equation is zero the pressure gradient is considered as:

\[ \frac{d\overline{P}}{d\tilde{t}} = \frac{2\overline{P}}{Re} \left( \frac{1}{2\pi n/3(3n+1)} \right) \]

(25)

The non-dimension pressure rise over a wave length is defined in the following form:

\[ \Delta \overline{P} = \int_0^L \overline{P} d\tilde{t} \]

(26)

And a relation is found for pressure rise in term of time-mean flow:

\[ \Delta \overline{P}_{\text{time-mean}} = 2 \frac{\lambda}{Re \epsilon} \left( \frac{1}{2\pi} \left( \frac{n}{3n+1} \right) \right) \]

(27)

**Solution Procedure (First-Order Approximation):** Assuming that there is no horizontal displacement of the tube walls during the peristaltic motion, by expanding the equations (13a,13b) about \( R=1 \) vertically, we have:

\[ \psi^{(1)} + \epsilon \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) - \psi^{(0)} (1) + \delta \psi^{(1)} + \frac{\delta^2}{2} \psi^{(2)} \]

(28)

\[ + \frac{\delta^3}{6} \psi^{(3)} + o(\delta^4) = 0 \]

(29)

Where:

\[ \delta = \epsilon \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

And the results are:

\[ \psi^{(1)} (1) \approx 0 \]

(30a)

\[ \psi^{(1)} (1) = -\psi^{(1)} (1) \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

(30b)

\[ \psi^{(1)} (1) = -\frac{1}{3} \psi^{(3)} (1) \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

(30c)

\[ \psi^{(1)} (1) = -\frac{1}{3} \psi^{(3)} (1) \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

(30d)

\[ \psi^{(1)} (1) = -\frac{1}{3} \psi^{(3)} (1) \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

(31)

These boundary conditions suggest that the solution for \( \psi \), can obtained in the following form:

\[ \psi (\frac{Z}{R}, \tilde{t}) = h(R) \cos \alpha (\frac{Z-\tilde{t}}{\lambda}) + g(R) \sin \alpha (\frac{Z-\tilde{t}}{\lambda}) \]

(32)

Eliminating the pressure gradient using cross-differentiation and subtraction of momentum equations then substituting \( \psi \) and \( \psi \) from equations (18, 32), afterward neglecting the coefficients of \( \epsilon^2 \) and \( \epsilon \alpha^2 \), we will have:
\[
\text{Re} \left[ -h \alpha \cos \left( Z - \frac{\tau}{2} \right) + g' \alpha \cos \left( Z - \frac{\tau}{2} \right) \right] + \text{Re} \left[ Bh \alpha \sin \left( Z - \frac{\tau}{2} \right) - \tilde{R} g \alpha \cos \left( Z - \frac{\tau}{2} \right) \right] + \text{Re} \left[ n + 1 \right] \left[ -h \alpha \cos \left( Z - \frac{\tau}{2} \right) + g' \alpha \cos \left( Z - \frac{\tau}{2} \right) \right] + \text{Re} \left[ n + 1 \right] \left( R^{(t-1)} - \tilde{R} \right) \times \\
\left[ -k \alpha \sin \left( Z - \frac{\tau}{2} \right) + g' \alpha \cos \left( Z - \frac{\tau}{2} \right) \right] + B^{(t-1)} \times R^{(t-1)} \right]
\]

\[
= \left( 1 - 2n \frac{h'}{R} \right) \left[ \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \left( 1 - 2n \frac{h'}{R} \right) \left[ \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \\
\frac{2(n-1)}{n} \left[ \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \frac{2(n-1)}{n} \left[ \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \\
\frac{2(n-1)}{n} \left[ \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \left[ 4 \frac{h'}{R} \cos \left( Z - \frac{\tau}{2} \right) + 4 \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] + \\
\frac{7}{15} \left[ \frac{2}{R} \cos \left( Z - \frac{\tau}{2} \right) + \frac{2}{R} \sin \left( Z - \frac{\tau}{2} \right) \right] - \frac{2}{R} \cos \left( Z - \frac{\tau}{2} \right) + 2 \frac{g'}{R} \sin \left( Z - \frac{\tau}{2} \right)
\]

By collecting the coefficients of sin and cosine in either side, two coupled equations are concluded as follows:

\[
\text{Re} \left[ g' \alpha \cos \left( Z - \frac{\tau}{2} \right) + n + 1 \right] B g' \alpha \cos \left( Z - \frac{\tau}{2} \right) + n + 1 \right] B g' \alpha \cos \left( Z - \frac{\tau}{2} \right) + \left[ R^{(1/2)} - \tilde{R} \right]
\]

\[
= B^{(t-1)} \times R^{(t-1)} \left[ -2n + 1 \left( \frac{h'}{R} \right) + 2 \left( n - 1 \right) \left( \frac{2h'}{R} - 2 \frac{h'}{R} + \frac{h}{R} \right) \right]
\]

And

\[
\text{Re} \left[ -h \alpha - n + 1 \right] B \alpha \cos \left( Z - \frac{\tau}{2} \right) + n + 1 \right] B \alpha \cos \left( Z - \frac{\tau}{2} \right) + \left[ R^{(1/2)} - \tilde{R} \right]
\]

\[
= B^{(t-1)} \times R^{(t-1)} \left[ -2n + 1 \left( \frac{g'}{R} \right) + 2 \left( n - 1 \right) \left( -2 \frac{g'}{R} + 2 \frac{g'}{R} + \frac{g}{R} \right) \right]
\]

With following boundary conditions based from equations (13a-13d):

\[
\begin{align*}
g' (0) &= 0 & h' (0) &= 0 & g (0) &= 0 & h (0) &= 0 \\
g' (1) &= -B & g (1) &= 0 & h (1) &= 1
\end{align*}
\]

The set of coupled ODE equations (34,35) are very complicated therefore the numerical spectral method based on Chebychev series is applied to obtain h, g and higher-order derivation of them.

Result and Discussion

The peristaltic motion of a power law fluid in a tube with a cosine wave propagating along the boundary has been considered under the assumption that the wave amplitude is small compared to half non-deformed diameter of flexible tube. The stream function and velocity components are obtained as power series, in terms of the amplitude of deformation divided by tube diameter. The Reynolds number is arbitrary but the flow remains laminar. It is imagined that the pressure changes linearly along the tube and it is uniform in each cross-section.

Figure 2 shows the variations of pressure difference versus time-mean flow rate over the wave period. As it is shown in Figure 2 the pressure rise decreases by increasing flow rate and the maximum flow rate is related to zero pressure rise. For Newtonian case (n=1) the diagram is linear as indicated by Merrone and Mazumdar [6]. Shear thinning fluid (n<1) diagrams are under the Newtonian fluid diagram with downward arc shaped as shown by Srivastava and Srivastava [7] but shear thickening fluid diagrams maintain on top of it with upward arc shaped. The diagrams show that in cases (n>1) the flow variation has small effect on pressure rise near to zero and it is vice versa for cases
(n<1). In both shear thinning and shear thickening fluid increasing power law index brings more pressure rise for the fixed time-mean flow rate.

Figures 3 and 4 show the pressure rise in term of time-mean flow rate for two different power law index (n=0.7 and n=1.5), in both diagrams increasing Reynolds number concludes higher pressure rise for the same time-mean flow rate therefore the definition of Reynolds indicates more pressure rise by increasing wave velocity, tube diameter and fluid density and also by decreasing power law index and fluid consistency.

Figure 5 shows the axial velocity profile in a fixed position for Newtonian and different non-Newtonian fluid. As it is shown all axial velocity profiles are parabolic form with zero tangent in the center line and the velocity reach to zero beside the wall. Increasing power law index results in higher velocity in the same radius of tube so there will be more flow rate for higher power law index fluid.

In Figures 6 and 7 the schematic of stream function ratio $\frac{\psi}{\psi_{wall}}$ is depicted in half upper-section of flexible tube in the wave frame for two different kind of fluid. There is a region where the stream lines are closed and make the torus-shaped eddy in the hyperspace of the tube. This phenomenon is called trapping. On increasing power law index these eddies change in shape, eddies are longer and thinner in shear thickening case compared to shear thickening case. Also boluses become smaller by increasing flow rate through the tube in both case and they disappear when flow rate reaches to infinity which refers to Stokes flow in the rigid cosine form tube (non-peristaltic flow). Siddiqui and Schwars [14] show the trend of eddy disappearance for second order fluid by increasing flow rate. The existence of eddies effects on flow behavior and make a bit phase shift on upper stream functions, especially for higher flow rate. The affection of eddy existence on stream line bend decrease to zero for the lower stream line and completely depends on the form and size of eddies.

Figures 8 and 9 shows the perturbation parameter affection on stream function and eddies made by closed stream lines for (n<1). It is clear that more amplitude of wave or less tube diameter made bigger torus-shaped eddy and the smaller perturbation parameter make straighter stream line. In case (b) and (c) the central stream functions are not completely straight whereas in case (a) these stream lines are straight and also there is no eddy because of less amplitude ratio. The similar results are shown in Figure 9 for (n>1). The comparison of Figure 8 and Figure 9 show that increasing power law index (n) make the bolus, shorter and wider and it is said before.
Conclusion

In this paper, the peristaltic flow of a power law fluid in a cylindrical channel is investigated by using a perturbation method in the wave frame. The effects of main parameters of flow rate, Reynolds number, flow behavior index (n) and amplitude ratio (ε) on the flow regime are studied. The results show that increment of power law index predicts more flow rate and less pressure rise in peristaltic motion. Trapping phenomenon is form by closed stream line depending on peristaltic motion.

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