Abstract

Mechanical loading has been shown to affect cell viability and matrix maintenance in the intervertebral disc (IVD) but there is no investigation on how cells survive mechanical stress and whether the IVD cells perceive mechanical loading as stress and respond by expression of heat shock proteins. This study investigates the stress response in the IVD in response to compressive loading. Bovine caudal disc organ culture was used to study the effect of physiological range static loading and dynamic loading. Cell activity, gene expression and immunofluorescence staining were used to analyze the cell response. Cell activity and cytoskeleton of the cells did not change significantly after loading. In gene expression analysis, significant up-regulation of heat shock protein-70 (HSP70) was observed in nucleus pulposus after two hours of loading. However, the expression of the matrix remodeling genes did not change significantly after loading. Similarly, expressions of stress response and matrix remodeling genes changed with application and removal of the dynamic loading. The results suggest that stress response was induced by physiological range loading without significantly changing cell activity and upregulating matrix remodeling. This study provides direct evidence on loading induced stress response in IVD cells and contributes to our understanding in the mechanoregulation of intervertebral disc cells.

Introduction

Degeneration of the intervertebral disc (IVD) is often associated with low back pain [1]. It affects a large number of people, reduces quality of life and causes economic loss. Studies on twins and genetics suggest that genetic factor play a major role in disc degeneration [2–4]. In addition to that, several factors have been suggested to contribute to the cause of the disease [5, 6]. Factors that are related to the patient conditions such as age and obesity as well as habit such as smoking were shown to be associated with disc degeneration [7, 8].

As IVD experience mechanical loadings during daily activities, extensive research has been done to elucidate the effects of mechanical loading on the IVD [9–12]. These studies show that high frequency and high magnitude compressive loading can cause cell death, catabolic gene
up-regulation and degeneration in IVD. However, it was unclear whether mechanical loading would cause cellular stress response in IVD.

Heat shock response is part of the cellular stress response, which acts as the cells’ protection and repair mechanism when triggered by environmental stressors such as heat, ultraviolet light, toxins, pH change and oxidative stress. Mechanical loading is also demonstrated to cause similar response. It has been demonstrated that stretching could induce Heat Shock Proteins (HSPs) upregulation in endothelial cells [13], melanocytes [14], bladder smooth muscle cells [15], vascular smooth muscle cells [16], periodontal ligament cells [17], trabecular meshwork cells [18] and tendon fibroblast [19]. Similar to the IVD, the articular cartilage is also subjected to considerable compressive loading. Expression of HSP70 was demonstrated to be up-regulated in human articular cartilage after static compression [20]. Similar findings were also reported in immortalized human chondrocytes in monolayer [21] and rabbit chondrocytes cultured in alginate beads [22] in response to high hydrostatic pressure. These results demonstrated that cells do respond to mechanical loading by upregulating HSP70.

Expression of HSPs has been shown in human IVD. Using histochemical study, HSP72 and HSP27 were found to accumulate in chondrocytes of endplate and nucleus pulposus in the IVD during childhood development but decrease with aging [23]. The percentage of HSP72 and HSP27 positive cells also increased in the degenerated IVD and HSP72 was identified specifically in the nuclei of these cells. The expressions of Heat Shock Factor-1 (HSF1), HSP72 and HSP27 were further found to be associated with cell cluster formation and other pathological conditions such as disc herniation [24]. The occurrence of HSPs in the degenerated disc was, therefore, suggested to be associated with disc degeneration. Nevertheless, to the best of our knowledge, there is to date no study available that demonstrates that cellular stress response is directly linked to mechanical loading.

In vitro organ culture using bovine caudal disc has been established and was used as a model for mechanobiology study previously [25–28]. Similarity in bovine disc dimension and cell popularity with human disc makes it an ideal model for mechanobiology study [25–30]. Here we hypothesized that compression loading in disc organ culture models stimulates stress responses of the disc cells. In this study, we specifically aim to investigate the effects of compression loading of different types and patterns on NP and AF. Stress responses and matrix remodeling will be studied at both gene and protein level.

Materials and Methods

Tissue culture

Fresh bovine caudal discs with endplate were harvested from eight one to two years old cows and cultured according to method previously described [31]. All experimental protocols were approved by the animal research committee of the University of Bern, Switzerland and the methods were carried out in accordance with the approved guidelines. In brief, after isolating the discs from the tail, the endplates were jet-lavaged with Ringer’s solution using Pulsavac wound debridement irrigation system to remove blood clots (Zimmer inc., Winterthur, Switzerland). Discs were then cultured in High glucose Dulbecco’s Modified Eagle’s Medium (DMEM, 4.5g/L glucose, Gibco, Life Technologies, inc., Basel, Switzerland) with 5% Fetal Calf Serum, 100 U/ml penicillin and 100 cg/ml streptomycin (all Sigma-Aldrich, Buchs, Switzerland).

Mechanical loading

As previous studies show that cell may react differently due to different loading types, cellular stress response in response to static and dynamic loading was studied. Bovine caudal discs
were loaded on to a custom made bioreactor [32] to apply compressive loading. IVD mechanobiology studies were previously performed on this bioreactor, which can maintain cell viability and nutrients diffusion throughout the experiment with dynamic compressive loads applied [30] (Fig 1). Loading pressure was calculated as force applied divided by the cross section area of the disc [30]. Compressive dynamic loading was applied at physiological range (0.35 ± 0.25 MPa, 0.2 Hz), while static loading was applied at 0.35 MPa for two h. Preliminary results showed that IVD cells had the highest up-regulation of HSP70 after two h of compressive loading compared to other time points. In order to study the temporal effect of the tissue after dynamic loading, cellular response after repeated loading was investigated. The discs underwent two h of dynamic loading, followed by 22 h of resting before a second round of loading.

Fig 1. Customized two degree-of-freedom (i.e., compression and torsion) bioreactor to maintain disc explants alive and to apply repeated mechanical loading for two days. A. close-up view of single station harboring a bovine coccygeal IVD soaked in culture media. Biocompatible materials are enox aluminium (black), polyoxymethylene (POM, white parts) and glass with a “press-fit” design and silicon rings (black rings) to ensure no leakage between glass and POM. B. 4-unit design arranged in 5% CO₂ and 60% humidity incubator. C. Scheme of control of uniaxial compression and axial torsion using fluidic muscle and servo-controlled valve. D. Close-up view of serrated titanium plate surface, which grasps IVD and keeps it in place and ensures nutrition diffusion to the bony endplate.

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resting cycle for two days (Fig 2). Samples were retrieved at different time points: right after loading and right after resting. Discs put under Heat-shock (43°C) treatment for two h were used as positive control. Free swelling discs cultured without any treatment were used as negative controls. Discs from the same animal were assigned to each condition to minimize inter-animal variability.

**Cell activity**

Cell activity was measured by resazurin assay that measures the aerobic respiration of the cells to assess cell viability [33]. Nucleus pulposus (NP) tissues and Annulus fibrosus (AF) tissues from each disc were incubated in medium with 50μM resazurin sodium salt (Sigma-Aldrich, Buchs Switzerland) for five hours. The relative fluorescence unit (RFU) was then measured using a spectrophotometer (SpectraMax M5, Molecular devices, distributed by Bucher Biotec, Switzerland). RFU measured for each tissue was normalized with the dry weight of the tissue.

**Relative Gene expression**

Total RNA was extracted by using TRI reagent. In brief, disc tissues were pulverized into powders in liquid nitrogen and homogenized with 1 mL TRI reagent (Molecular Research Center,

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**Experimental conditions**

**A. Heat shock:**
1. Control
2. HS (42°C)

**B. Loading modes:**
1. Control (w/o Loading)
2. SL (Static loading, 0.35MPa)
3. DL (Dynamic loading, 0.35±0.25MPa)

**C. Repeated loading:**
1. Control
2. DL
3. DL+Rest
4. DL*2
5. DL+Rest*2

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**Fig 2. Conditions applied to disc explants.** Heat-shock was applied on discs as positive control (A). Compressive loading of different modes was applied at physiological range 0.35 MPa (static loading) and 0.35 ± 0.25 MPa (dynamic loading) for two h (B). For repeated loading, compressive dynamic loading was for two h per day for two days (C). Samples were retrieved for analysis at different time points: 1. Control, 2. DL (right after two h of dynamic loading), 3. DL+Rest (22 h after dynamic loading), 4. DL*2 (right after two h of dynamic loading on Day two), 5. DL+Rest*2 (22 h after dynamic loading on Day two).

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RNA extracted was then purified using GenElute Mammalian total RNA purification kit followed by DNA digestion (Both from Sigma-Aldrich, Buchs, Switzerland). Reverse transcription was carried out by using iScript cDNA Synthesis kit (Bio-Rad, Reinach, Switzerland). Oligonucleotide primers for qPCR were designed by Beacon Designer™ (Premier Biosoft inc., Palo Alto, CA) based on sequences from NCBI GenBank database. The information of the primers is presented in Table 1. Quantitative PCR was performed on an iQ5 qPCR Detection System (Bio-Rad). Every reaction consisted of 2 μL water, 5 μL iQ-SYBR Green Super mix (Bio-Rad, Cressier, Switzerland), 1 μL primers (0.25 μM) and 2 μL cDNA. All C_t values of the genes were normalized to C_t value of ribosomal 18S RNA. Fold change of the gene expression was calculated relative to the negative control group from the same animal by 2^-ΔΔCt method.

Actin and immunofluorescence staining

Tissues were fixed in freshly-prepared 4% buffered paraformdehyde, frozen and cryo-sectioned for immunofluorescence staining. Sections of 10 μm were stained with primary antibodies of mouse monoclonal anti-HSP72 (inducible form of HSP70, at 1:100 dilution, ADI-SPA-810, Enzo, NY) and rat monoclonal anti-HSF1 (at 1:50 dilution, ab61382, Abcam, Cambridge, MA). Briefly, sections were hydrated in phosphate buffered saline solution (PBS) and permeabilized with 0.5% Tween-20 (Sigma-Aldrich, Buchs, Switzerland). Antigen was retrieved in citrate buffer (10 mM sodium citrate with 0.05% Tween-20 at pH 6.0) at 95°C for 15 min and then washed with 0.05% Tween-20. Blocking was done using 3% bovine serum albumin (Jackson Immuno Research, PA) for 30 min. Sections were then incubated with primary antibodies at 4°C for overnight. After washing with PBS, sections were then incubated in appropriate fluorochrome conjugated secondary antibodies at 1:400 dilution for 1 h. For actin staining, sections were incubated in rhodamine-phalloidin (Molecular Probes, Eugene, OR) at 1:40 dilution for one h. The sections were mounted with Fluoro-Gel II with DAPI (EMS, Hatfield, PA). Images were scanned using a confocal scanning microscope (LSM700, Carl Zeiss, Jena, Germany). Signal intensity of HSP70 and HSF1 in each nucleus was quantified using IMARIS software (Bitplane AG, Zurich, Switzerland) and normalized to the volume of the nucleus.

Statistical analysis

All statistical analyses were executed using SPSS 19.0 (IBM, NY). The significance level was set to 0.05. Non-parametric analysis of variance by rank test (Kruskal-Wallis test) was use to test significant difference between loaded groups and control. One-way ANOVA was performed to determine significant difference of cell activity among multiple groups.

Table 1. Primers used for quantitative real time PCR in organ culture study.

| Gene | Forward Primer (5’ - 3’) | Reverse Primer (5’ - 3’) |
|------|--------------------------|-------------------------|
| 18S  | ACG GAC AGG ATT GAC AGA TTG | CCA GAG TCT CGT TCG TTA TCG |
| HSP70| AGG AGG TGG ATT AGG AAT GGA CAG TTC AAC ATC TCA |
| HSF1 | GCA GGT GTT CAT AGA ATT GTA TT | CTG GCT CAT CGG TCT GTT |
| ACAN | GCC ATC GTG TCC CAT TAC AG | ACT CGT CCT CGT TCC CAT AG |
| COL2 | CGG GTG AAC GTG GAG AGA CA | GTC CAG GGT TGC CAT TGG AG |
| COL1 | GCC TCG CTC ACC AAC TTC | AGT AAC CAC TGC TCC ATT CTG |
| ADAMTS4 | TCC TGG CTG GCC TCC TCT TC | CCT CGG ACA AGT CTT CAG AAT CTC |
| MMP3 | CTT CCG ATT CTG CTG TCT AGG | AGT GTG TCT TCG TCC TCT G |
| MMP13 | TCC TGG CTG CCT TCC TCT TC | CCT CGG ACA AGT CTT CAG AAT CTC |

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Results

Cell activity and cytoskeleton

Fig 3 shows that cell activity was maintained under all conditions with no significant reduction of cell viability (One way ANOVA, p > 0.05). F-actin of the cells did not change substantially after heat-shock and loading with no stress fibers observed after loading.

Fig 3. Cell activity and cytoskeleton were maintained after each condition. Cell activity was measured by resazurin assay (A-B) and cytoskeleton was visualized by f-actin staining (C-J) for NP and AF after each condition. Values are normalized to control without loading and represented in mean ± SEM.

Control: Control discs without loading, HS: Heat-Shock, SL: Static Loading, DL: Dynamic loading, DL+Rest: Dynamic loading with Resting, DL*2: dynamic loading for two days, DL+Rest*2: dynamic loading and resting for two days. NP: Nucleus pulposus, AF: Annulus fibrosus. N = 5. RFU: relative fluorescence unit.

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Heat-shock
Heat-shock was used as the positive control to assess cells’ ability to upregulate expression of HSPs. Gene expression of HSP70 and HSF1 were analyzed as both are involved in cellular response towards stresses including heat stress and mechanical stress [34, 35]. Heat-shock stress resulted in a 100-fold increase in HSP70 in both NP and AF (S1 Fig). Kruskal-Wallis test showed that the upregulation in HSP70 was statistically significant different in both NP (p = 0.002) and AF (p = 0.001) compared to negative control. On the other hand, there was no statistical significant difference in the expression of HSF1, which is the transcription factor for HSP70, HSF1 in both NP and AF.

Different loading types
Fig 4 shows the gene expressions of the tissues under different loading types under three groups of genes: stress response genes (Fig 4A–4D: HSP70 and HSF1), matrix anabolic genes (Fig 4E–4J: ACAN, COL2 and COL1) and matrix catabolic genes (Fig 4K–4P: ADAMTS4, MMP3 and MMP13).

HSP70 was up-regulated in NP after static and dynamic loading (Fig 4A) by about 2.8 and 2.4-fold respectively. Statistical testing using Kruskal-Wallis test revealed significant upregulation in expression of HSP70 of NP in response to static loading (p = 0.047) and dynamic loading (p = 0.029). Expression of HSP70 in AF did not change after static loading and was up-regulated very little with considerable variation after dynamic loading (Fig 4C). Expression of HSF1 (Fig 4B & 4D) did not show any significant difference between the loading types and control for both NP and AF.

Expression pattern of matrix remodeling genes were generally similar in NP and AF. The changes in expression of matrix anabolic genes in NP were not statistical significant. In AF, Kruskal-Wallis test demonstrates significant up-regulation in ACAN (p = 0.010) and COL2 (p = 0.047) after static loading compared to control. For gene expression of matrix catabolic genes under different loading types, ADAMTS4 and MMP13 in NP did not change much after dynamic loading (Fig 4K & 4M), whereas MMP3 expression (Fig 4L) was up-regulated by about 10-fold after static loading but was not statistical significant different. In AF tissue, ADAMTS4 expression was significantly down-regulated by about 9-fold in response to static loading (p = 0.028) but not dynamic loading (Fig 4N).

Repeated loading
Changes in expression of HSP70 in response to dynamic loading were transient (Fig 6A). Up-regulation continued to be observed 22 h after loading at day two (p = 0.005) compared to control. Similar trend was observed in HSF1 expression (Fig 6B). On the other hand, AF had a different expression trend from NP. Expression of HSP70 was only up-regulated at day 1 both right after loading and 22 h after loading but dropped to basal level at day 2 (Fig 6C) but without any significant differences.

Expression of ACAN appeared to be up-regulated right after each round of loading and down-regulated 22 h after loading in both tissues (Fig 6E & 6H). Expression of COL2 was up-
Fig 4. Relative gene expression after different loading types. Gene expressions are in log of fold change normalized to control without loading and represented in means ± SEM. SL: Static Loading, DL: Dynamic Loading.

* = statistical significant difference with p < 0.05. N = 5 (from 3 animals) compared to control.

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regulated mildly in the DL + Rest+2 group of NP (Fig 6F, p = 0.005) compared to control. In contrast, expression of COL1 did not significantly change (Fig 6G & 6J). For matrix catabolic genes, expression of ADAMTS4 did not show significant changes (Fig 6K & 6N). Expression of MMP3 showed a similar trend in NP and AF, which increased significantly in response to dynamic loading in day 1 (p = 0.005) and decreased after resting in day 2 (Fig 6L & 6O). Resting for 22 h after first round of loading upregulated MMP13 in NP by about 15-fold (Fig 6M, p = 0.005).

It is also notable that expressions of HSP70 (NP), HSF1 (NP), ACAN (NP and AF) and COL2 (AF) showed an oscillating trend with up-regulation right after loading and down-regulation after resting. In contrast, ADAMTS4 (NP) and MMP13 (NP) show opposite expression trend with up-regulation after resting.

Discussion

Studies have investigated different aspects on how the IVD cells respond towards loading but none of them explored the stress response of the IVD cells in situ. Expression of HSPs had been associated with disc degeneration, pathology and aging [23, 24]. The association was suggested to be related to mechanical and environment stress experienced by the cells but there is no study that demonstrates the direct causal relationship of mechanical stress and expression of HSPs in IVD cells in their native ECM environment. Using organ culture, the results from the current study provide more evidence to this suggestion by demonstrating NPCs’ expression of HSP70 in response to repetitive cyclic compressive loading. This finding suggests that healthy NPCs activate relevant stress response to cope with mechanical stress.
Throughout the study, disc cell’s activity was maintained in all conditions, confirming that cell viability was not affected by short-term heat-shock nor compression. This is consistent with earlier results using similar magnitude of loading [30]. Both magnitudes were suggested to be in physiological range for large animal discs such as ovine [36, 37] and bovine discs [30].

Compressive loading appears to induce stress response in NPCs, even though only a relatively low physiological range magnitude was applied and cell activity was not altered. Heat-shock response was seen in NPCs under both static loading and dynamic loading but the fold change in response to compression is much lower than heat-shock, which was also reported in chondrocytes [35]. This effect was continually observed when the tissues were loaded for a second time under dynamic loading. The expression trend appears to oscillate with loading and resting. This further indicates that the major heat shock protein, HSP70 exclusively up-regulates after loading, while cells recover after rested. The other two heat shock proteins, HSP27 and HSP90 were only upregulated insignificantly in response to dynamic loading (S2 Fig). On the other hand, up-regulation of HSP70 after loading was not observed in AFCs. This suggests that the deformation of the AFCs surrounding extra cellular matrix is smaller and the matrix shielded AFCs from mild mechanical stress under compression.

Mechanism and cell signaling pathway linking cells mechanical loading to cell fate is not fully understood. Reasons of mechanical loading caused stress response have been speculated previously. It was suggested that stress response is caused by cytoskeleton reorganization and protein synthesis due to mechanical loading [35, 38, 39]. Loading induced expression of HSP70 was further suggested to be leading to stress fiber formation. By using inhibitor, the study showed that inhibition of HSP70 would prevent HSP70 up-regulation and stress fibers formation after stretch. In contrast, disrupting formation of stress fibers had no effect on HSP70 up-regulation [13]. The authors hypothesized that cytoskeleton reorganization maybe an outcome rather than a cause of up-regulation of HSP70. In this study, substantial cytoskeleton reorganization was not observed with up-regulation of HSP70, supporting the hypothesis. Cytoskeleton reorganization may only happen with longer loading duration. On the other hand, global protein synthesis was demonstrated to be suppressed during loading and rebound after loading withdrawal [40]. This leads to a theory that stress response occurs as part of the chaperone activity due to protein synthesis [19, 35, 38, 41]. Besides, loading induced stress response is suspected to be a downstream event of the mechanotransduction pathway. Several mechanosensors were suggested to induce cellular stress responses. For example, stretch-activated ion channels were demonstrated to activate HSF1 and up-regulate HSP70 [42] while integrins were suggested to be coordinated with cellular stress response [43]. Expression of HSP70 involved in mechanical loading related chaperone activity and mechanotransduction pathway needs to be elucidated in future experiments.

The majority of the matrix remodeling genes, which include the matrix anabolic and catabolic genes were mildly up-regulated after static loading and dynamic loading. This finding is rather consistent with existing literature using bovine caudal disc model that most of the matrix remodeling genes were upregulated mildly for both tissues [30]. Significant up-regulation of ACAN and COL2 after dynamic loading and down-regulation of ADAMTS4 after static loading in AFCs suggest physiological range compression signals the AFCs to inhibit the matrix remodeling genes.
catabolic process and maintain the extracellular matrix. The results agree with existing literature that physiological range loading is more favorable for matrix maintenance of the disc [11, 12, 36]. Another study observed up-regulation of COL2 and ACAN in NPCs for a longer duration (> 7 days) of dynamic loading using caprine disc [36]. This was not observed in NP in this study, suggesting that the short-term loading (2 days) may not be enough to upregulate the matrix anabolic genes. However, dynamic loading appears to be more favorable to the matrix production in both NP and AF tissue.

Oscillating up- and down-regulation trends with loading and resting suggest that changes in expression of matrix remodeling genes in IVD cells were transient as demonstrated in earlier studies [44–46]. However, the trends of matrix anabolic and catabolic genes were different compared to the mentioned studies due to different models and experimental conditions. In this study, the anabolic and catabolic genes present opposite trend which suggest a different peak of mRNA expression may follow after loading.

Mechanism to link the expression of HSP70 to matrix maintenance has been demonstrated in cartilage and chondrocytes, where expression of HSP70 was shown to induce matrix production and prevent matrix degradation [47–49]. The observation in this study, up-regulation of HSP70 in NP without significant matrix remodeling, suggests that stress response is more likely to be induced before matrix remodeling and hence may be a downstream event of mechano-transduction pathway. The relationship between such cellular pathways and matrix remodeling mechanisms in response to loading needs further investigation.

**Conclusion**
This study investigated the stress response of the IVD towards mechanical loading. Compressive loading induced stress response was demonstrated in bovine caudal disc. Up-regulation of HSP70 was observed in the NPCs during compressive loading at physiological range, where cell activity was not changed and matrix remodeling was low.

**Supporting Information**
S1 Fig. Relative gene expression of stress response genes after heat-shock. Gene expressions are in log of fold change normalized to control without loading and represented in mean ±SEM. HS: Heat-Shock. * = statistical significant difference with p<0.05 compared to control. N = 5.

S2 Fig. Relative gene expression of HSP27 and HSP90 in response to different loading types. Gene expressions are in log of fold change normalized to control without loading and represented in means ± SEM. SL: Static Loading, DL: Dynamic Loading, N = 5 (from 3 animals) compared to control.

**Author Contributions**
Conceived and designed the experiments: WHC SCWC BG BPC.
Performed the experiments: WHC SCWC.
Analyzed the data: WHC SCWC BG BPC.
Contributed reagents/materials/analysis tools: BG BPC.
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