INTRODUCTION

The kernel regression algorithm includes two algorithms: traditional kernel regression (CKR) and controlled kernel regression (SKR),\(^1\)\(^-\)\(^3\) used for medical image processing and image reconstruction, demonstrating good denoising effects and edge preservation effects.\(^4\)\(^-\)\(^6\) However, the calculation process is complicated.
During image reconstruction algorithm, the function is introduced to automatically extract the features of the image data, and the optimized internal parameters have higher accuracy and reliability. In this study, three-dimensional transperineally ultrasound was used to evaluate the effect of caesarean delivery and caesarean section on ASC.

**METHODS**

Oner hundred fifty seven primiparas who were postnatally reviewed in our hospital from September 2018 to December 2020 were selected after IRB approval (Dated March 23, 2021), aged 25 to 40 years old, with an average of (29.3 ± 2.8) years; 77 of them were in labour delivery (shun delivery group) and 80 were in caesarean delivery (Caesarean section group).

**Inclusion criteria:** 1. Single pregnancy, ultrasound in the second trimester confirmed that the foetus size is consistent with gestational week; 2. Underwent three-dimensional transperineally ultrasound examination 42 days after delivery; 3. No history of pelvic surgery. In the perinatal group, 36 patients received perineal side resection and one patient had forceps delivery; none of the women in the caesarean section group entered the second stage of labour. There was no statistically significant difference in maternal age, height, bodyweight at delivery and birth weight of new-borns between the two groups (all P>0.05), Table-I.

The use of GE Coulson E8Expert ultrasound diagnostic apparatus, cavity volume probe, frequency 5 ~ 9MHz. Instruct the subject to defecate and urinate before the inspection. During the examination, the subject was instructed to take the lithotomy position, hip flexion, and mild knee abduction. Place the probe on the perineum of the patient, take a cross-section, scan from the end of the anus to the anorectal angle, and observe the ASC in multiple planes. 1. The proximal plane, the IAS plane adjacent to the distal end of the anorectal angle; 2. The central plane, the PRM surrounds the IAS at the rear and shows the clearest plane; 3. The distal plane, at the same time clearly shows the plane of the IAS and EAS. Measure the thickness of IAS at 3, 6, 9, and 12 o’clock in the above three planes, and measure the thickness of EAS at 3, 6, 9, and 12 o’clock in the far plane.

**Statistical analysis:** Use SPSS20.0 statistical analysis software. Independent sample t-test was used to compare the thickness of ASC in different directions and the general conditions of maternal and new-born between the caesarean section and the caesarean section group. P<0.05 was considered statistically significant. In the CPU version of the nuclear regression reconstruction algorithm, the algorithm itself is divided into two parts: data acquisition and target volume reconstruction.

After entering the initial filling stage, discrete three-dimensional ultrasound graphic data will be obtained as shown in Fig.1. The various points in this graphic can be expressed by the formula under non-parametric estimation:

![Fig.1. Three-dimensional figure of human organs. (a) Initial filling stage. (b) Regression stage.](image-url)
where $Y_i$ is the observed value, $r(\cdot)$ is the regression equation (cannot be determined), $X_i = (X_{i1}, X_{i2}, X_{i3})^T$ is the three-dimensional coordinate of the corresponding point, $\varepsilon_i$ is the noise error of the constant distribution that does not interfere with each other, $1 \sim P$ represents all points in the three-dimensional graph. It can be seen that $r(X_i)$ is assumed to be the actual value of the 3D ultrasound graph here, however, this particular function cannot be determined. Here we continue to assume that the $r(X_i)$ function is locally N order derivable. For any point X in the three-dimensional ultrasound graph, to estimate the value of the ultrasonic graph here, however, this particular function is now a function with the influence of point $X$ (calculation point), and $\beta$ is assumed to be the actual value of the 3D coordinate of the corresponding point, only when $r(X_i)$ is close to point $X$, the resulting regression equation is closer to 0, the resulting regression equation is closer to the true value. In order to solve this optimization problem, the least squares equation is used here:

$$Y_i = r(X_i) + \varepsilon_i, i = 1, 2, L, P$$  \hspace{1cm} (1)

The above shows that if the Taylor function is regarded as the local performance of the regression function, the estimated parameter $\beta_n$, in equation (2) can be expressed as the estimated solution of the regression equation when the data is $X_i$.

To make the observed value $Y_i$ closer to the value of the regression equation $r(X_i)$, only when $\varepsilon_i$ is closer to 0, the resulting regression equation is closer to the true value. In order to solve this optimization problem, the least squares equation is used here:

$$\min_{|X_i|} \sum_{i=1}^{L} \left[ Y_i - \beta_0 - \beta (X_i - X)^T - \beta_1 (X_i - X)^T - L - \beta_0 (X_i - X)^T \right]^2 \cdot K_h (X_i - \frac{X}{h})$$ \hspace{1cm} (3)

Where $K(\cdot)$ is a kernel function and a weight function, used to determine the influence of the points around the calculation point on the calculation point. To control this influence. In particular, function $K(\cdot)$ is a symmetric function, and its maximum value is 0, which satisfies:

$$\int_{\mathbb{R}^3} K(t) dt = 0, \int_{\mathbb{R}^3} t^2 K(t) dt = 0$$ \hspace{1cm} (4)

Here $c$ is a constant value. The function $K(\cdot)$ selected here is usually a Gaussian function, but it can also be other forms of functions, as long as the above constraints are satisfied. In the literature on non-parametric statistics, the most widely considered are local constants, linear and quadratic approximations. The corresponding values of N are 0, 1, and 2, respectively, This paper chooses the case where N is 2.

The kernel function $K(\cdot)$ is now a function with three directional variables, and its bandwidth $h$ should be a 3 * 3 matrix. However, usually the covariates of each scale have the same mean and variance. To simplify the problem, only the bandwidth $h$ in all directions is considered here, and then the Gaussian function selected is:

$$h^3 K \left( \left\| \frac{X_i}{h} \right\| \right) \hspace{1cm} (5)$$

Where $h$ is the bandwidth of the Gaussian function and the smoothing parameter introduced earlier. As a three-dimensional point $X$, there is $X = (X_1, X_2, X_3)^T$. For more convenient calculation, let N take the value of 3, taking into account the situation of the three-dimensional point, the formula (3) Equivalent transformation into

$$\sum_{j=1}^{3} W_i (X) \left( Y_j - \beta_0 - \sum_{j=1}^{3} \beta_j (X_i - X_j)^2 \right)^2 \hspace{1cm} (6)$$

Here $W_i (X)$ represents the influence of point $X_i$ on the central point X (calculation point), and its value is determined according to the distance from point $X_i$ to point X and the corresponding bandwidth $h$, expressed as:

$$W_i (X) = K \left( \left\| \frac{X_i - X}{h} \right\| \right) \hspace{1cm} (7)$$

To facilitate the operation of the computer, it is necessary to convert the minimum case of equation (6) to the form of a matrix. For each point around the calculation point, there is a distance matrix $X_x$ to store the distance from the surrounding points to the calculation point. The matrix is as follows:

$$X_x = \begin{bmatrix} 1 & X_{11} - X_1 & X_{12} - X_2 & X_{13} - X_3 \\ X_{11} - X_1 & 1 & X_{12} - X_2 & X_{13} - X_3 \\ X_{11} - X_1 & X_{12} - X_2 & 1 & X_{13} - X_3 \\ X_{11} - X_1 & X_{12} - X_2 & X_{13} - X_3 & 1 \end{bmatrix} \hspace{1cm} (8)$$

This matrix is also the distance matrix that the CPU needs to prepare for GPU operations when the GPU algorithm is implemented later. This matrix will be further introduced in subsequent articles.
Suppose, when formula (6) obtains the minimum value, the corresponding value of $\beta_0, \beta_1, \beta_2, \beta_3$ is:

$$\hat{\beta} = \left( \beta_0, L, \beta_3 \right)^T$$  \hspace{1cm} (9)

Assuming that the estimated value is $\hat{r}(X)$, according to the $\hat{\beta}_0$ mentioned above, it is the estimated value sought in this article, it is not difficult to obtain:

$$\hat{r}(X) = \hat{\beta}_0$$  \hspace{1cm} (10)

RESULTS

One child in the perinatal group showed a continuous interruption of EAS after three months of perineal ultrasound (Fig.2). The results of the three groups of three-dimensional ultrasound measurement of perineal thickness of the two groups of IAS, EAS and PRM are shown in Table-II and Table-III. The thickness of the IAS proximal plane 6, 12 o’clock direction and the central plane 9 and 12 o’clock direction of the obstetric group were less than that of the caesarean section group (all $P <0.05$).

DISCUSSION

Obstetric anal sphincter injury occurs during delivery. Thinning of EAS will weaken the function of ASC. After delivery, IAS and EAS become thinner. Any injury of EAS, PRM, and IAS is closely related to incontinence in the anus. Meriwether et al. used transanal ultrasound and transperineal ultrasound for examinations, and the results showed that, the left PRM of normal women was thicker than the right. Johannessen et al. proposed that, changes in hormones, neuromuscular, and mechanics during pregnancy played a more important role in the basin function damage than vaginal delivery. In the study, it was found that the delivery method has a certain

| Group                      | IAS proximal plane | IAS mid-plane |
|----------------------------|-------------------|--------------|
|                            | 3 o’clock 6 o’clock 9 o’clock 12 o’clock | 3 o’clock 6 o’clock |
| Natural birth group (n = 77) | 2.05±0.54 1.86±0.53 2.15±0.57 1.53±0.60 | 2.25±0.58 1.83±0.55 |
| Caesarean Section (n = 80)  | 2.21±0.67 2.11±0.76 2.17±0.58 1.78±0.55 | 2.40±0.59 1.73±0.48 |
| t value                    | 1.6 2.32 0.21 2.7 | 1.61 -1.19 |
| P value                    | 0.11 0.02 0.83 <0.01 | 0.11 0.23 |

| Group                      | IAS mid-plane | IAS far plane |
|----------------------------|--------------|---------------|
|                            | 9 o’clock 12 o’clock 3 o’clock 6 o’clock 9 o’clock 12 o’clock | |
| Natural birth group (n = 77) | 2.33±0.51 1.65±0.63 2.13±0.60 2.04±0.59 2.23±0.51 1.55±0.56 |
| Caesarean Section (n = 80)  | 2.53±0.61 2.01±0.57 2.19±0.59 1.98±0.57 2.37±0.54 1.72±0.60 |
| t value                    | 2.31 3.7 0.68 -0.76 1.67 1.82 |
| P value                    | 0.02 <0.01 0.5 0.45 0.1 0.07 |
Table-III: Comparison of thickness measurements between the distal EAS plane and the central plane of the caesarean and caesarean section.

| Group                      | EAS far plane | PRM Midplane |
|----------------------------|---------------|--------------|
|                            | 3 o’clock  | 6 o’clock  | 9 o’clock | 12 o’clock | 4 o’clock | 8 o’clock |
| Natural birth group (n = 77)| 2.93±0.82 | 2.04±0.59 | 3.12±0.84 | 1.04±0.27 | 7.00±1.40 | 7.21±1.39 |
| Caesarean Section (n = 80)  | 2.87±0.80 | 2.73±0.88 | 3.23±0.77 | 1.87±0.55 | 7.37±1.51 | 7.34±1.71 |
| t value                    | -0.52      | -0.48      | 0.8       | 12.15      | 1.62      | 0.55      |
| P value                    | 0.6        | 0.63       | 0.43      | <0.01      | 0.11      | 0.58      |

impact on the shape of the anal sphincter complex. In this study, the perineum of the delivery group and the caesarean section group was thicker than that of the natural delivery group at the proximal plane of IAS at 3, 6 and 9 o’clock.

The kernel regression image algorithm mainly uses the kernel regression interpolation function for non-parametric estimation. In terms of image noise reduction, image fusion, and image interpolation, this algorithm has good denoising and interpolation effects. Takeda et al.11 applied the kernel regression algorithm to image noise reduction. Compared with the traditional method, the image edge preservation effect and the image interpolation effect were both significant. Ultrasound is widely used in the clinic to detect the perineum. The main imaging methods for evaluating the sphincter complex are transrectal ultrasound and magnetic resonance imaging. Ultrasound imaging can present a 360-degree cross-section of anal sphincter. The anal sphincter is evaluated factoring into the proximal plane, the middle plane and the distal plane.12,13 To use kernel regression algorithm to process the ultrasound image effectively removes the blurred image and improves the diagnosis accuracy. Compared with the traditional image, the three-dimensional image in this research was clearer. Stuart et al.15 performed transperineal ultrasound imaging on women undergoing the repair of obstetric sphincter injury six months before. The images obtained were clear whether in contracted or resting state.

Rectal ultrasound is the gold standard for diagnosing anal sphincter injury. Some scholars believe that, the ultrasound probe will compress the anal sphincter to a certain extent and affect the measurement to a certain extent. Transperineal ultrasound is reduces the deformation of the anus, and the three-dimensional tea-red color is the basin imaging diagnosis mode. Williams et al.16 found that, three-dimensional ultrasound and 3D technology imaging had a high degree of conformity in the measurement of EAS, and the IAS contour on the 3D image was clear. In this study, tomography and volume contrast imaging were used to observe the morphology and integrity of the anal sphincter complex. The delivery group had thinner distal anal sphincter at 12 o’clock, proximal anal sphincter at 6 and 12 o’clock, and central plane at 9 and 12 o’clock versus the C-section group. There was a significant difference between the two groups (P<0.05). There was no significant difference in the thickness of the remaining internal and external sphincter muscle and puborectalis in different directions between the two groups (P>0.05). The defect of the patient’s vaginal sphincter can be found by three-dimensional ultrasound of the perineum.

**CONCLUSION**

PRIM is considered to be another important organizational structure that maintains anal self-control functions in addition to IAS and EAS. Anal sphincter injury is related to PRM injury, and there are many common risk factors for the injury of the two, and the use of forceps to assist labour in normal labour is the most important factor. At present, it is generally accepted that, compared with caesarean section, caesarean delivery has a greater impact on the elevator ani muscles. In this study, there was no statistically significant difference in thickness between the 4 and 8 o’clock planes of the central plane of the caesarean section and the caesarean section. However, there are deficiencies in this study, such as limited sample size, failure to analyse the relationship between ASC thickness and anal incontinence, etc, to be further studied in the future.
REFERENCES

1. Siu KL, Yuen KS, Castaño-Rodriguez C, Ye ZW. Severe acute respiratory syndrome coronavirus ORF3a protein activates the NLRP3 inflammasome by promoting TRAF3-dependent ubiquitination of ASC. FASEB J. 2019;33(8):8865-8877. doi: 10.1096/fj.201802418R

2. Dick MS, Sborgi L, Ruhl S, Hiller S, Broz P. ASC filament formation serves as a signal amplification mechanism for inflammasomes. Nat Commun. 2016;7:11929. doi: 10.1038/ncomms11929

3. Friker LL, Scheiblich H, Hochheiser IV, Brinkschulte R. β-Amyloid Clustering around ASC Fibrils Boosts Its Toxicity in Microglia. Cell Rep. 2020;30(11):3743-3754.e6. doi: 10.1016/j.celrep.2020.02.025

4. Vourtsis A. Three-dimensional automated breast ultrasound: Technical aspects and first results. Diagn Interv Imaging. 2019;100(10):579-592. doi: 10.1016/j.diii.2019.03.012

5. He XF, Zeng YY, Li G, Feng YK. Extracellular ASC exacerbated the recurrent ischemic stroke in an NLRP3-dependent manner. J Cereb Blood Flow Metab. 2020;40(5):1048-1060. doi: 10.1177/0271678X19856226

6. Guo R, Lu G, Qin B, Fei B. Ultrasound Imaging Technologies for Breast Cancer Detection and Management: A Review. Ultrasound Med Biol. 2018;44(1):37-70. doi: 10.1016/j.ultrasmedbio.2017.09.012

7. Poon LC, Sahota DS, Chaemsaiathon P, Nakamura T, Machida M. Transvaginal three-dimensional ultrasound assessment of Sylvian fissures at 18-30 weeks’ gestation. Ultrasound Obstet Gynecol. 2019;54(2):190-198. doi: 10.1002/uog.20172

8. den V. Noort F, Grob ATM, Slump CH, van der. Vaart. CH, van, Stralen. M. Automatic segmentation of puborectalis muscle on three-dimensional transperineal ultrasound. Ultrasound Obstet Gynecol. 2018;52(1):97-102. doi: 10.1002/uog.18927

9. Meriwether KV, Hall RJ, Leeman LM, Migliaccio L. Anal sphincter complex: 2D and 3D endoanal and translabial ultrasound measurement variation in normal postpartum measurements. Int Urogynecol J. 2015;26(4):511-7. doi: 10.1007/s00192-014-2524-5

10. Johannessen HH, Wibe A, Stordahl A, Sandvik L, Morkved S. Anal incontinence among first time mothers - what happens in pregnancy and the first year after delivery? Acta Obstet Gynecol Scand. 2015;94(9):1005-1013. doi: 10.1111/aogs.12689

11. Takeda H, Farsiu S, Milanfar P. Deblurring using regularized locally adaptive kernel regression. IEEE Trans Image Process. 2008;17(4):550-63. doi: 10.1109/TIP.2007.918028

12. Billard JM, Freret T. Asc-1 transporter activation: an alternative to rescue age-related alterations in functional plasticity at rat hippocampal CA3/CA1 synapses. J Neurochem. 2018;147(4):514-525. doi: 10.1111/jnc.14586

13. Shah SWH, Butt AK, Malik K, Alam A, Khan AA. Pneumatic balloon dilatation for achalasia cardia; early & late results, a single center study. Pak J Med Sci. 2017;33(5):1053-1058. doi: 10.12669/pjms.335.13685

14. Zarin M, Khan M, Ahmad M, Ibrahim M, Khan MA. VAAFT: Video Assisted Anal Fistula Treatment; Bringing revolution in Fistula treatment. Pak J Med Sci. 2015;31(5):1233-1235. doi: 10.12669/pjms.315.6836

15. Stuart A, Ignell C, Orno AK. Comparison of transperineal and endoanal ultrasound in detecting residual obstetric anal sphincter injury. Acta Obstet Gynecol Scand. 2019;98(12):1624-1631. doi: 10.1111/aogs.13701

16. Williams AB, Bartram CI, Halligan S, Marshall MM. Endosonographic anatomy of the normal anal canal compared with endocoil magnetic resonance imaging. Dis Colon Rectum. 2002;45(2):176-83. doi: 10.1007/s10350-004-6140-1

Author’s Contribution:

NH conceived the study, literature search, data analysis drafting the manuscript.

LS helped in design, data collection, drafting of paper & critical revision , is also accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved.

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