Dense movement with embedded sparse action-type representations in the output layer of motor cortex

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Abstract:
Motor cortex generates output necessary for the execution of a wide range of motor behaviours. Although neural representations of movement have been described throughout motor cortex, how population activity in output layers relates to the execution of distinct motor actions is less well explored. To address this, we imaged layer 5B population activity in mice performing a two-action forelimb task. We found most neurons convey a generalised movement signal, with action-type-specific signalling restricted to relatively small, spatially intermingled subpopulations of neurons. Deep layer population dynamics largely reflect dense, action-invariant signals that correlate with movement timing, while embedded sparse action-type representations reflect distinct forelimb actions. We suggest that sparse coding of action-type enhances the number of possible output configurations necessary for behavioural flexibility and the execution of a wide repertoire of behavioural actions.

Introduction:
Descending motor commands originating in deep layers of motor cortex propagate to subcortical, brainstem and spinal cord circuits to initiate a large repertoire of movements (Brecht et al., 2004; Cheney and Fetz, 1980; Esposito et al., 2014; Lawrence and Kuypers, 1968; Lemon, 2008; Miri et al., 2017; Omrani et al., 2017; Wang et al., 2017; Yakovenko and Drew, 2015). In primates and rodents, disrupting cortical output directly affects limb coordination and timing (Brochier et al., 1999; Brown and Teskey, 2014; Galiñanes et al., 2018; Guo et al., 2015; Lawrence and Kuypers, 1968; Morandell and Huber, 2017; Ueno et al., 2018), while stimulation evokes a range of complex motor actions (Ferrier, 1873; Graziano et al., 2002; Harrison et al., 2012; Hira et al., 2015; Li and Waters, 1991). The firing rates of individual neurons in motor cortex correlate with various aspects of limb movement such as joint angle, direction, and speed (Georgopoulos et al., 1982; Moran and Schwartz, 1999; Paninski et al., 2004; Thach, 1978), while population activity likely reflects multiplexed sensorimotor signals necessary for coordinating evolving movement trajectories (Ames et al., 2019; Churchland et al., 2012; Hatsopoulos et al., 2007; Kaufman et al., 2016; Sauerbrei et al., 2019). Functional maps of motor cortex have been generated for forelimb reach (Amirikian and Georgopoulos, 2003; Georgopoulos et al., 2007; Harrison et al., 2012; Hira et al., 2015; Wang et al., 2017), rhythmic movements (Dombeck et al., 2009; Hira et al., 2015) and object manipulation (Hira et al., 2013). Despite this, we still do not fully understand the extent to which distinct motor actions are represented in the output layers of motor cortex or how this information is spatiotemporally organised.

Recent advances in viral tools and optical imaging have enabled access to laminar-specific spatiotemporal dynamics of interconnected neuronal populations in rodent motor cortex (Park
et al., 2019; Peters et al., 2014; Peters et al., 2017; Wang et al., 2017). During the execution of single forelimb actions, principal neurons in both superficial and deep layers display dense activity patterns that causally relate to the initiation and/or ongoing evolution of movements (Dacre et al., 2019; Estebanez et al., 2017; Hira et al., 2013; Isomura et al., 2009; Levy et al., 2020; Park et al., 2019; Sauerbrei et al., 2019; Wang et al., 2017). These reproducible, laminar-specific activity patterns emerge across motor learning and correlate with enhanced limb coordination (Laubach et al., 2000; Masamizu et al., 2014; Peters et al., 2014; Peters et al., 2017). But whether deep layer cortical activity patterns represent specific actions or a more generalised motor signal is still in debate. For example, mice performing skilled reaches with a single endpoint trajectory display dense motor cortex activity with >70% of neurons encoding task-related movement (Sauerbrei et al., 2019), whereas multi-directional centre-out forelimb reaches appear to be encoded by sparse action-specific activity in superficial layers (Galiñanes et al., 2018). To address this issue, we sought to investigate how action representations are organised in one of the main output layers of primary motor cortex, layer 5B, since its output targets subcortical, brainstem and spinal cord circuits necessary for the selection and execution of motor actions (Esposito et al., 2014; Kita and Kita, 2012; Shepherd, 2013; Wang et al., 2017).

We performed deep-layer 2-photon calcium imaging in the caudal forelimb area (CFA) of mice trained to perform an alternating abduction / adduction lever task. By combining population imaging with single neuron / population-based classifiers and dimensionality reduction, we show that layer 5B neurons display dense movement but sparse action-type representations. Neurons conveying action-type-specific information displayed uncorrelated activity patterns that spanned the entire movement period and were spatially intermingled within forelimb motor cortical microcircuits. Our findings have important implications for understanding the functional organisation and coding of action-specific information in the output layers of rodent motor cortex.

Results
To explore different models of action representation (Figure 1A) (Dombeck et al., 2009; Galiñanes et al., 2018; Harrison et al., 2012; Hira et al., 2015; Sauerbrei et al., 2019), we first developed a cued linear abduction / adduction lever task for mice. The task design, incorporating two diametrically opposing actions (abduction – extension of the forelimb away from the body vs adduction – retraction of the limb towards the body), required mice to push or pull a horizontal lever 4 mm upon presentation of a 6 kHz auditory cue (Figure 1B and C). By incorporating two opposing actions we aimed to maximise differences in forelimb biomechanics, muscle activation and neural activity patterns (Georgopoulos et al., 1982). Mice
rapidly learned the task (mean = 12.8 days, 95% CI [11.3 14.2]), all data, unless otherwise stated, are presented as mean, [bootstrapped 95% confidence interval] and average data is given per mouse, N = 12 mice), performing sequences of abduction / adduction movements with reproducible across-session success but differences in kinematic trajectories, reflecting two independent actions (abduction – 41.3 trials / 30 min [37.5 45.2], median action duration = 713.5 ms, 95% CI [706.5, 733.5]; adduction – 42.3 trials / 30 min [38.4 45.9], median action duration = 566 ms 95% CI [537.3, 573.0], N = 12 mice) (Figure 1D – F and Supplementary Video 1). To confirm motor cortical output was required for both actions, we focally injected the GABA_A receptor agonist muscimol centred on the caudal forelimb area (Dacre et al., 2019; Schiemann et al., 2015). By applying muscimol during behavioural engagement we could assess the immediate effects of CFA inactivation 5-15 mins after drug injection (Figure 1G). Muscimol rapidly blocked initiation of both actions, reducing overall task success by ~65%, an
effect that persisted for the duration of the session before recovering after 24 hours (5-15 mins, abduction - normalised task success = 0.34 [0.22 0.47], N = 6 mice, F(1,2) = 2.25, P = 1.4x10^{-2}, two-way ANOVA; addition – normalised task success = 0.35 [0.20 0.53], N = 6 mice F(1,2) = 1.62, P = 3.2x10^{-3}, two-way ANOVA; adduction – normalised task success = 0.34 [0.22 0.47], N = 6 mice, F(1,2) = 2.25, P = 1.4x10^{-2}, two-way ANOVA; abduction – normalised task success = 0.35 [0.20 0.53], N = 6 mice). Blocking cortical output resulted in either monoparesis of the contralateral forelimb (i.e. localised weakness without complete loss of function) or an inability to initiate learned movements, both of which affected successful task completion (Supplementary Video 2).

To examine how output from motor cortex relates to the execution of distinct motor actions, we imaged behaviour-related population activity in layer 5B of motor cortex, the upper boundary of which was identified by the presence of pyramidal tract neurons (boundary ≥500 μm from the pial surface at the centre of CFA) (Schiemann et al., 2015) (Figure 2A and B and Supplementary Figure 1). A large proportion of layer 5B neurons displayed movement-related activity changes (468 / 653 neurons, 73.5 % [64.7 81.8] per field-of-view (FOV) from 12 FOVs, N = 6 mice; see Methods) the remainder being classified as non-responsive (147 / 653 neurons, 20.9 % [12.8 29.1] per FOV) or ‘reward phase’ neurons (38 / 653 neurons, 5.7 % [3.7 7.7] per FOV) (Figure 2C and D). By separating abduction and adduction trials, we found that most layer 5B neurons displayed movement-related activity changes that were indistinguishable between actions (287 / 468 neurons, median = 59.8 %, interquartile range (IQR) [42.9 74.3], N = 6 mice), with only a small fraction of neurons distinguishing action type (termed action bias, abduction bias – 81 / 468 neurons, median = 14.3 %, IQR [12.7 28.6]; addition bias – 100 / 468 neurons, median = 11.8 %, IQR [8.2 27.7]) (Figure 2E and F). Neural responses displaying action bias were classified into six different types including both positive and negative changes in ∆F/F₀, consistent with bidirectional action-specific tuning of neural activity (Georgopoulos et al., 1982). The majority of action bias neurons (76%) showed significant changes in ∆F/F₀ for both actions, while only 24% (43/181 neurons) displayed action selectivity (i.e. significant change in ∆F/F₀ for one action, with no response for the opposing action) (Supplementary Figure 2A). In terms of spatial organisation, action bias neurons were found in all FOVs and were spatially intermingled with non-bias neurons (Figure 2F and G). Although our task design required mice to execute actions from two different starting positions, action bias was in general not driven by postural differences (seen as differences in inter-trial baseline ∆F/F₀) but rather reflected the type of movement being executed (Supplementary Figure 2B and C). To challenge our physiology-based classification of action bias, we adopted an unbiased, data-driven approach using a Gaussian Naïve Bayes classifier to identify whether action type could be decoded from the activity of individual layer 5B neurons (Figure 2H and I). We found that ~70% of neurons that displayed action bias had decoding accuracy scores above chance (122 / 181 neurons, median = 67.3 %, IQR [42.6
N = 6 mice) (Figure 2J), with a small minority of non-action bias neurons also representing action type. Consistent with our physiology-based classification, neurons with above chance decoding accuracy were found in the majority of FOVs, were spatially intermingled with other cell types and represented a small fraction of the total population of neurons with movement-related activity (124 / 468 neurons, median = 27.1 %, IQR [11.8 51.0], N = 6 mice) (Figure 2K and L). Together, our data suggest that most layer 5B neurons convey a generalised action-invariant motor signal, whereas a small fraction of neurons convey action-specific information.
Given the high trial-to-trial variability in $\Delta F/F_0$ and resultant moderate decoding scores in individual neurons (see Figure 2I), we reasoned that population responses could provide a more robust movement-related signal that would enhance decoding of action type (Levy et al., 2020; Masamizu et al., 2014; Wei et al., 2019). By applying logistic regression (Figure 3A), population decoding was consistently more accurate when compared to decoding from single neurons (single cell median decoding accuracy $= 0.61$, IQR [0.58 0.65]; population median decoding accuracy 0.75, [0.63 0.79], N = 6 mice, W = 1, Z = -2.2, $P = 2.8 \times 10^{-2}$, Wilcoxon signed rank test) (Figure 3B). However, this increase was driven by a small proportion of neurons with high decoding accuracy. Removing the top $\sim 20\%$ of neurons based on single
cell decoding accuracy abolished action-type classification (median prop. removed = 0.21, [0.11 0.61], N = 6 mice) (Figure 3C-D and F), whereas, sequential removal of randomly selected neurons resulted in a significantly larger proportion of neurons having to be removed before decoding accuracy reduced to chance (median prop. removed = 0.64, [0.41 0.98], N = 6 mice, W = 1, Z = -2.2, \( P = 2.8 \times 10^{-2} \), Wilcoxon signed rank test) (Figure 3E and F). To further explore the underlying structure of layer 5B population activity, we employed principal component analysis (Churchland et al., 2012; Churchland et al., 2010; Cunningham and Yu, 2014; Kaufman et al., 2014; Stopfer et al., 2003). For the leading 16 principal components of the population activity, we compared the difference between abduction and adduction trials, in order to compute a discrimination index (d’) (Figure 3G and Supplementary Figure 3). Leading principal components tended to be more similar across actions, while action type was often better represented by higher components (Figure 3G). Despite correlating with population decoding scores, high d’ values were not preferentially associated with the leading principle components of the population activity (Supplementary Figure 3), suggesting action-type is not a dominant signal in the population response (Kaufman et al., 2016). We explored this further by comparing d’ scores following sequential removal of individual neurons. Removing the top ~15% of neurons based on single cell decoding accuracy abolished action-type discrimination (median prop. removed = 0.15, [0.05 0.47], N = 6 mice) (Figure 3H & J), whereas, the random removal of neurons required a significantly larger proportion of the population to be removed before d’ values reduced to chance (median prop. removed = 0.35, [0.11 0.85], N = 6 mice, W = 1, Z = -2.2, \( P = 3.1 \times 10^{-2} \), Wilcoxon signed rank test) (Figure 3I & J). Together, these results indicate that while action-type can be decoded from population activity, this is dependent on a relatively small proportion of high decoding accuracy neurons that contribute a small proportion of the overall variance.

Functional clustering of neurons appears to be a common feature of population activity in motor cortex (Amirikian and Georgopoulos, 2003; Cheney et al., 1985; Dombeck et al., 2009; Georgopoulos et al., 2007; Harrison et al., 2012; Hira et al., 2013; Hira et al., 2015; Isomura et al., 2009; Jones and Wise, 1977; Komiyama et al., 2010; Wang et al., 2017). We examined the spatiotemporal organization of high decoding accuracy neurons and found that within each FOV the onset of \( \Delta F/F_0 \) changes were first observed ~300 ms prior to movement, consistent with a role in preparation / initiation (Dacre et al., 2019; Estebanez et al., 2017; Isomura et al., 2009; Li et al., 2015a), and tiled the movement period up to reward delivery (~1-1.5 s; abduction – high decoding accuracy neurons median \( \Delta F/F_0 \) onset = 119 ms, IQR [83.3 142.9], range [-875 1450]; adduction – 167 ms, [95.2 177.4], -925 1350], N = 6 mice). However, neurons with different \( \Delta F/F_0 \) onsets appeared spatially heterogenous (Figure 4A and B). To explore correlations in peri-movement activity patterns, we split neurons based on their
Figure 4: Heterogeneous spatiotemporal organisation of high decoding accuracy neurons.

(A) Example field-of-view (FOV) showing spatial distribution of ∆F/F onsets for high decoding accuracy neurons during abduction trials. MI, movement initiation. Colours represent 200 ms bins filling the peri-movement epoch: -100 ms (light orange) to +1100 ms (dark brown). (B) Left, cumulative probability plots of ∆F/F onsets for high decoding accuracy (HDA, orange) and low decoding accuracy neurons (LDA, grey) from the example FOV shown in (A). Right, histograms of ∆F/F onsets for HDA and LDA neurons during abduction (top) and adduction (bottom) trials (n = 12 FOVs, N = 6 mice). (C) Modelled functional network depicting HDA neurons with correlated (top left) or uncorrelated (top right) activity. Each node, represented by a circle, corresponds to a neuron, while the connections represent the strength of activity correlation between neurons. Bottom left, functional network constructed from the pairwise activity correlations from a representative FOV. Bottom right, box-and-whisker plots showing the median, interquartile range and range of correlation coefficients across mice for HDA (orange), LDA (grey) and all (brown) neurons. Black dots represent correlation values for individual mice. Line colour (light to dark) and width correspond to increasing values of Pearson’s r. Neurons are plotted as nodes in Euclidean space with colour (HDA - orange, LDA - grey) and size relating to increasing decoding accuracy (n = 468 neurons from 12 FOVs, N = 6 mice). (D) Left, distributions of pairwise correlation coefficient for HDA (orange) and LDA (grey) neurons. Right, median pairwise correlation coefficient with 95% CI as a function of pairwise distance for HDA (orange) and LDA (grey) neurons. Horizontal lines denote linear regression model fit, with shaded regions representing the bootstrap 95% CI (P < 0.19, 95% CI [-0.033, 0.014], n = 11594 observations, N = 6 mice). (E) Modelled functional network depicting clustered (top left) and spatially heterogeneous (top right) HDA neurons. Each node, represented by a circle, corresponds to a neuron, while the connections represent the pairwise distances between neurons. Bottom left, functional network constructed from the pairwise distances between neurons in a representative FOV. Bottom right, box-and-whisker plots showing the median, interquartile range and range of pairwise distances across mice for HDA (orange), LDA (grey) and all (brown) neurons (n = 468 neurons from 12 FOVs, N = 6 mice). Black dots represent pairwise distances for individual mice. (F) Revised model of layer 5B movement representations in caudal forelimb motor cortex (CFA). Coloured circles represent non-responsive (grey), movement-responsive (violet), abduction biased (purple) and adduction biased (blue) neurons.

decoding accuracy scores (high, low and all) and compared pairwise activity during abduction or adduction trials observing only weak correlations within and across groups (Figure 4C and Supplementary Figure 4). Next, we compared the activities of pairs of neurons as a function of their pairwise distance. Neurons separated by less anatomical distance did not show correlated ∆F/F changes, suggesting an absence of functional clustering (Figure 4D and E). Confidence intervals provide a lower bound indication of cluster size such that, if present, spatial clusters based on decoding accuracy would have to be less than ~50µm. Thus, layer 5B neurons that convey action-type information appear to be temporally and spatially heterogeneous.

Discussion

Volitional forelimb movements are thought to be represented by relatively dense activity patterns in both superficial and deep layers of motor cortex (Dacre et al., 2019; Estebanez et al., 2017; Hira et al., 2013; Isomura et al., 2009; Levy et al., 2020; Park et al., 2019; Sauerbrei et al., 2019; Wang et al., 2017), but whether these patterns represent specific actions (Galiñanes et al., 2018) or a more generalised motor signal (Kaufman et al., 2016) remains unresolved. By combining population imaging with single neuron / population-based classifiers and dimensionality reduction in mice, we find that most layer 5B neurons display action-invariant signalling, while action-specific representations are restricted to sparse, spatially heterogeneous subpopulations of neurons. Our findings provide constraints on models of
spatiotemporal movement representations (Figure 4F), developing our understanding of how action-specific information is organized in the output layers of motor cortex.

In rodents, volitional forelimb movements such as reach-to-grasp (Estebanez et al., 2017; Galiñanes et al., 2018; Guo et al., 2015; Levy et al., 2020; Sauerbrei et al., 2019; Wang et al., 2017) or pulling/pushing a grasped lever (Dacre et al., 2019; Hira et al., 2013; Isomura et al., 2009; Miri et al., 2017; Morandell and Huber, 2017; Park et al., 2019) have been associated with widespread, bidirectional neuronal modulation in both superficial and deep layers of sensorimotor cortex, driven by long-range inputs from motor thalamus (Dacre et al., 2019; Sauerbrei et al., 2019; Tanaka et al., 2018). Both excitatory and inhibitory neurons display dense task-related activity which emerges across learning and correlates with enhanced limb coordination (Hwang et al., 2019; Laubach et al., 2000; Masamizu et al., 2014; Peters et al., 2014). Disrupting this activity affects limb kinematics suggesting dense cortical activity may be a common cortical motif representing specific motor actions (Gao et al., 2018; Guo et al., 2015; Li et al., 2015b; Sauerbrei et al., 2019). Our data challenge this view, in that most layer 5B neurons display similar activity patterns irrespective of action-type, indicative of a more generalised motor signal that conveys information necessary for movement, but not for specific actions. Action-invariant signals likely provide a generic timing signal, triggering state-dependent switching from stable neural dynamics during rest towards oscillatory dynamics that underpin movement initiation and execution (Churchland et al., 2010; Kaufman et al., 2014; Kaufman et al., 2016; Kurtzer et al., 2005) and similar to condition-invariant population transitions observed in recurrent neural networks trained to recapitulate complex muscle patterns in reaching primates (Sussillo et al., 2015). Since the cerebellar thalamocortical pathway conveys timing signals, which when disrupted affects movement initiation (Dacre et al., 2019; Sauerbrei et al., 2019; Thach, 1978), action-invariant signalling in cortex could reflect a generic broadcast signal from the cerebellum signalling the intention to move, irrespective of action type. This broadcast signal likely combines with long-range action-specific inputs targeted to specific subpopulations of neurons to generate embedded sparse action-type representations. In addition, action-invariant signalling may also provide online input to downstream subcortical controllers to ensure maintained limb position in the absence of motor commands necessary for executing volitional movements (Albert et al., 2020; Kaufman et al., 2016). It will be interesting in the future to apply methods to selectively disrupt action-dependent and action-invariant signalling to explore their contribution to postural control and limb kinematics across multiple distinct actions.

Within layer 5B, we found that decoding of action-type was restricted to a subpopulation of neurons which could reflect routing of action information through specific output channels
What is the computational advantage of sparse action representations as a coding strategy? In deep layers of cortex, intratelencephalic neurons constitute a major source of input to the dorsolateral striatum controlling action selection and vigour (Panigrahi et al., 2015; Park et al., 2020; Shepherd, 2013; Yttri and Dudman, 2016), while pyramidal tract neurons project to brainstem (Esposito et al., 2014) and spinal cord circuits involved in movement execution (Basista and Yoshida, 2020; Cheney and Fetz, 1980; Economo et al., 2018; Ueno et al., 2018; Wang et al., 2017). Flexible, sparse recruitment, via long-range inputs (Hooks et al., 2013) and hierarchical input-output connectivity (Kiritani et al., 2012; Shepherd, 2013; Weiler et al., 2008) of intratelencephalic and pyramidal tract neurons conveying action-specific information
would greatly enhance the number of possible output configurations necessary to realise a large repertoire of kinematic representations. Our work suggests that deep-layer sparse cortical representations embedded within dense action-invariant signalling may be an organising principle that could ensure behavioural flexibility across motor actions. Further work exploring how sparse cortical codes influence downstream motor areas will be essential for understanding how cortex controls the planning and execution of distinct motor actions.

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Author contributions

Methods
Animal husbandry and general surgery
Male adult C57BL/6J wild-type mice (5-12 weeks old, 20-30g, 1-4 animals per cage) were maintained on a reversed 12:12 hour light:dark cycle and provided ad libitum access to food and water as well as environmental enrichment. All experiments and procedures were
approved by the University of Edinburgh local ethical review committee and performed under license from the UK Home Office in accordance with the Animal (Scientific Procedures) Act 1986. Surgical procedures were performed under ~1.5% isoflurane anaesthesia and each animal received fluid replacement therapy (0.5ml sterile Ringer’s solution), buprenorphine (0.05 mg/kg) and either carprofen (4 mg/kg) or dexamethasone (2 mg/kg) for pain relief and to reduce inflammation. At 24 and 48 hours Carprofen (4 mg/kg) was administered for post-operative pain relief. Craniotomies, centred on 1.6 mm lateral, 0.6 mm rostral relative to bregma, were performed in a stereotactic frame (David Kopf Instruments, CA, USA) using a hand-held dentist drill with 0.5 mm burr. A small lightweight headplate (0.5 g) was implanted on the surface of the skull using cyanoacrylate glue and dental cement (Lang Dental, IL, USA) and mice were left for at least 48 hours to recover.

**Behavioural training**

After recovery from head plate surgery, mice were handled extensively before being head restrained and habituated to a custom forelimb lever abduction-adduction behavioural setup. Mice were trained to perform two diametrically opposing movements - a 4mm abduction (extension of the forelimb away from the body) or adduction (retraction of the forelimb towards the body) - in response to a 6 kHz auditory cue to obtain a water reward (~5 µl). To increase task engagement, mice were placed on a water control paradigm (1 ml/day) and weighed daily to ensure body weight remained above 85% of baseline. Mice were trained once per day for 30 mins and advanced through different phases of the task once they achieved at least 50 rewards in each of two consecutive sessions. Initially, mice were required to perform uncued abduction and adduction movements to obtain rewards, prior to the introduction of an auditory cue with pseudo-random inter-trial-interval (ITI) of 6-8s and a response window of 10 s window. The response window was gradually reduced to 2 s across training sessions.

**Forelimb kinematic tracking**

A motion index was calculated from high speed videos (60fps, Prosilica GC780C, Allied Vision, Germany or 300 fps for *in vivo* pharmacology, Mako U U-029, Allied Vision) of mouse behaviour acquired using Streampix 7 (Norpix, Canada). A rectangular region of interest (ROI) was drawn around the left forelimb and the frame-to-frame difference in pixel intensity was calculated using the formula: 

\[ MI_f = \sum_{i=1}^{N}(c_{f+1,i} - c_{f,i})^2, \]

where \( c_{f,i} \) is the grayscale level of pixel \( i \) in the frame \( f \). Motion index was aligned to behaviourally-relevant time points (lever displacement, cue presentation etc), with videos and behaviour resampled to a common sampling rate. Motion index onsets were calculated by aligning the smoothed traces (40-point
loess filter) to the lever movement and identifying the last point prior to movement where mean motion index was > threshold (mean upper bound of 95% confidence interval during baseline).

**In vivo pharmacology**
Mice trained to expert level had a small burr hole opened directly above caudal forelimb area (CFA; 1.6 mm lateral, 0.6 mm rostral to bregma) before recovering for > 90 mins. After 10 min of behaviour, the lever was locked and a small volume of the GABA receptor agonist muscimol (200nl of 2mM stock dissolved in external saline solution containing 150 mM NaCl, 2.5 mM KCl, 10 mM HEPES, 1.5 mM CaCl, and 1 mM MgCl₂, adjusted to pH 7.3) or saline (vehicle only) was injected into the target area (AP: 0.6, ML: 1.6, DV: -0.7 mm). Behavioural metrics were analysed from 10 mins post injection and the experimenter was blinded to drug versus control groups.

**Retrograde tracing**
To selectively label pyramidal tract (PT-type) neurons in layer 5B of CFA, red RetroBeads (Lumafluor, USA) were injected into the pons (4.0 mm caudal and 0.4 mm lateral of bregma), delivered via pulled glass pipettes (5μl, Drummond Scientific, PA, USA; 10-20 nl/min) using an automated injection system (Model Picospritzer iii, Parker, NH, USA). Injections were made at 4 sites (100 nl / site) located 200, 400, 600 and 800 μm dorsal from the cranial floor. After > 14 days post-injection, mice were terminally anaesthetized using an intraperitoneal injection of a ketamine/domitor mixture (75 mg/kg ketamine, 1 mg/kg domitor) and transcardially perfused with 30 ml of phosphate-buffered saline (PBS) followed by 30 ml of 4% paraformaldehyde (PFA, Sigma-Aldrich, MO, USA), dissolved in PBS and adjusted to pH 7.4. Brains were post-fixed at 4 °C for 1-3 days in 4% PFA solution, then transferred to PBS solution. Individual brains were cut into coronal sections (60 μm) using a vibrating microtome (Leica VT1200 S, Leica Microsystems (UK) Ltd.), mounted with Vectashield Antifade Mounting Medium (Vector Laboratories, CA, USA) and sealed with a glass coverslip. Images were acquired with a Leica DM R epifluorescence microscope and image analysis was performed using ImageJ (Rueden et al., 2017) and MATLAB (MathWorks, MA, USA). To obtain estimates of the depth of layer 5B in CFA, 3 coronal sections from each brain were imaged (0.54 mm, 0.6 mm and 0.66 mm rostral to bregma). Brightness/contrast adjustments and background subtraction (rolling ball, 30 pixels wide at 1.28 μm/pixel; Fiji (Schindelin et al., 2012) functions were performed to reduce the contribution of background autofluorescence. Each ROI was then divided into 25-μm-deep bins that were normalised to a value between 0 and 1, with 0 being the darkest bin and 1 being the brightest bin and all bins were compared to baseline. In order to obtain a depth profile of layer 5B within CFA, the depth of the dorsal-most retrogradely
labelled neuron was recorded at 100 µm intervals from 1.3 - 1.9 mm lateral of bregma and repeated in 5 sequential coronal sections from 0.36 - 0.84 mm rostral of bregma. For each mouse, the depth of layer 5B at the centre of CFA (1.6 mm lateral, 0.6 mm rostral to bregma) was taken as the reference depth and the depths of other locations reported relative to this value.

**Immunohistochemistry**

Mice expressing GCaMP6s were transcardially perfused and horizontal sections (30 µm) were cut parallel to the surface of CFA. Sections were rinsed in PBS overnight, incubated with a blocking solution (PBS, with 0.5% Triton X-100 (Sigma-Aldrich) and 10% goat serum (Sigma-Aldrich)) for 2 hrs and rinsed with PBS. Sections were incubated overnight with mouse anti-NeuN (MAB377 Anti-NeuN Antibody, clone A60, Sigma-Aldrich) diluted 1:1500 in carrier solution (PBS, with 0.5% Triton X-100 and 1% goat serum), then rinsed with PBS. For secondary antibody binding, sections were incubated overnight with goat anti-mouse Alexa Fluor 568 (Invitrogen, MA, USA) diluted 1:750 in carrier solution then rinsed with PBS. Sections were mounted onto glass slides, briefly air-dried, covered with Vectashield Antifade Mounting Medium (Vector Laboratories), and sealed with a glass coverslip. Images of CFA were acquired using a Nikon A1R FLIM confocal microscope (20X objective lens, 0.8 NA, Plan Apo VC, Nikon, Europe). Three images were taken at imaging planes corresponding to layer 5B (550 µm from the cortical surface). The number of cells in each image was manually counted and divided by the area to obtain a measure of neuron density. For most fields-of-view (FOVs) recorded during calcium imaging, neurons were not visible in all portions of the frame due to occlusion by blood vessels. Polygons were drawn around visible neurons in each field-of-view to provide a realistic estimate of the imaging area.

**2-photon imaging**

To perform population calcium imaging in layer 5B of CFA, 200 nl of AAV1-SynGCaMP6s (2.9x10^13 GC/ml, Addgene 100844-AAV1) was injected into contralateral motor cortex (AP: 0.6, ML: 1.6, DV: 0.6 mm) via pulled glass pipettes (5 µl, Drummond Scientific; 10-20 nl/min) using an automated injection system (Model Picospritzer iii, Parker), before sealing the craniotomy with silicone (Body Double; Smooth-On, PA, USA) and implanting a lightweight headplate. For imaging a cranial window, a glass coverslip (#0; Menzel-Gläser, Germany; 2-photon imaging) was fixed in place with cyanocrylate glue was implanted above the virus injection site. 2-photon calcium imaging was performed using a custom-built resonant scanning 2-photon microscope (320 x 320 µm field-of-view; 600 x 600 pixels) with a Ti:Sapphire pulsed laser (Chameleon Vision-S, Coherent, CA, USA; < 70 fs pulse width, 80 MHz repetition rate) tuned to 920 nm wavelength. Images were acquired at 40 Hz with a 40x
objective lens (0.8 NA; Nikon) with custom-programmed LabVIEW-based software (LotoScan). Motion artefacts in the raw fluorescence videos were corrected using discrete Fourier 2-dimensional-based image alignment (SIMA 1.3.2; (Kaifosh et al., 2014)). ROIs were drawn manually in Fiji and pixel intensity within each ROI averaged to produce a raw fluorescence time series (F). To remove fluorescence originating from neuropil and / or neighbouring neurons, fluorescence signals were decontaminated and extracted using nonnegative matrix factorisation, as implemented in FISSA (Keemink et al., 2018). Normalized fluorescence was calculated as $\Delta F/F_0$, where $F_0$ was calculated as the 5th percentile of the 1Hz low-pass filtered raw fluorescence signal and $\Delta F = F - F_0$. All further analyses were performed in custom written scripts in MATLAB or Python v 3.7, freely available via the Duguid Lab GitHub repository (https://github.com/DuguidLab). In order to define movement-related neurons, we first defined a baseline (-1.5 to -0.5 s relative to motion index onset) and peri-movement (-0.15 s from motion index onset to +1.5 s after lever movement) epochs. Movement-related neurons were identified by two independent methods: 1) bootstrapped distribution (10,000 samples) of baseline-to-peak values (mean of the 100ms centred on the largest deviation from baseline within the peri-movement epoch - mean of baseline epoch) were compared with the baseline – traces were smoothed with a 40 frame loess filter; 2) bootstrapped distributions of $\Delta F/F_0$ in 250 ms bins within the peri-movement epoch were compared with baseline. If either method identified significant differences the neuron was classified as movement-related. $\Delta F/F_0$ onsets were calculated using a previously published onset detection algorithm using a slope sum function (SSF; (Zong et al., 2003)) with the decision rule and window of the SSF adapted to calcium imaging data (threshold 10% of peak, SSF window 375 ms, smoothed with a Savitzky Golay filter across 27 frames with order 2) and reported as the median of 10,000 bootstrapped samples to reduce the influence of noisy individual trials. Neurons with onsets beyond the peri-movement window were defined as ‘reward phase’ neurons. Neurons with action bias were detected using the same classification criteria described above but across actions (i.e. significant differences in bootstrapped $\Delta F/F_0$ baseline-to-peak or 250ms peri-movement bins).

**Neural decoding**

To decode action-type in single neurons we employed a Naïve Bayes classifier, where distributions of features are assumed to be Gaussian. Motion index-aligned $\Delta F/F_0$ data were assessed within a 10 s peri-movement window to produce a time series for the decoding accuracy. At each time point, leaving one trial out (test trial), the likelihood of determining abduction or adduction was based on the remaining trials (training set). For cross-validation, the leave-one-out procedure was then repeated by looping over trials. The resulting decoding accuracy time series were analysed within a peri-movement epoch - the peri-movement epoch
began at -0.15 s relative to motion index onset and ended based on the peak $\Delta F/F$ response of each neuron; the position of the median peak was calculated for each action type and the later of these time points used as the cut off. To identify neurons with decoding performance above chance, the bootstrapped distributions of decoding accuracy scores were compared against a threshold value for each session. Only neurons with at least 1 bin significantly higher than threshold were defined as high decoding accuracy. The threshold for each session was calculated based on modelled data composed of random samples from a Gaussian distribution with the same number of trials as the experimental data. For each session, modelled data accuracy was calculated 1000 times, assuming a prior probability of 50:50, and the mean ± 2 SD was used as the threshold for significance. For population level classification of action type, we employed logistic regression. As above, the decoding accuracy of time series for each population was generated via leave-one-out design looped over all the trials in a given session. Population decoding accuracy was defined as the maximum decoding accuracy in any 250 ms bin within the peri-movement epoch. Population decoding was also performed on subsets of the entire population. Neurons were removed from the population one at a time, either in order from highest to lowest decoding accuracy score or randomly. The process was repeated 25 times in the random condition and the median of all responses used as the representative example for comparison with the ordered removal condition. Subpopulations of neurons decoding significantly above chance were determined by comparing decoding scores with a shuffled dataset (sampled randomly from 1000 time points with the trial labels (abduction or adduction) randomised for each sample). If confidence intervals from the population data did not overlap with those of the shuffled data, population scores were deemed to be above chance. In 3/12 FOVs with low proportions of high decoding neurons and trial numbers, the population decoding accuracy was never significantly above chance. These FOVs were excluded from the comparison between ordered and random removal of neurons.

**Dimensionality reduction**

Raw fluorescence traces for all trials with successful movements in a 7.5 s peri-movement window were concatenated, filtered with a three frame (120 ms) wide boxcar kernel, whitened and transformed with principal component analysis. The principal components (PCs) corresponding to the 16 highest eigenvalues, which corresponded to an average 83% (range 77%, 94%) cumulative explained variance, were analysed. To compute trajectories in PC space, PC projections for all trials were averaged (separately for abduction or adduction) and the variance and 95% confidence intervals for each time point estimated via 100-fold bootstrapping. The separability of the trajectories for abduction or adduction was computed in each PC separately as $d'(t) = |m_{\text{ab}}(t) - m_{\text{ad}}(t)| / \sqrt{0.5(v_{\text{ab}}(t) + v_{\text{ad}}(t))}$, where $m_{\text{ab}}(t)$ and $m_{\text{ad}}(t)$
are the mean trajectories for abduction and adduction, and \( v_{\text{abd}}(t) \) and \( v_{\text{add}}(t) \) the corresponding variances, estimated from trials. The separability \( d'(t) \) was bootstrapped from 200 samples, and variance and 95% confidence intervals estimated from this sample. \( d'(t) \) was computed for all frames from movement onset to termination, where the latter was the longest time of movement execution recorded in each session. PCs were considered separable if the difference between \( d'(t) \) and \( d_{\text{shuffle}}'(t) \) (obtained in the same way from trial-shuffled data) was within the 95% confidence interval, which was estimated from the sum of the relevant bootstrapped variances. For each FOV, the largest significant \( d'(t) \) was used; in 2/13 FOVs no PCs showed significant separability (these two FOVs also had a chance level population decoding score), and were excluded in the summary data.

**Spatiotemporal organisation**

To assess the functional (temporal) organisation of simultaneously recorded populations of neurons, pairwise correlation coefficients (Pearson’s \( r \)) from the motion index-aligned \( \Delta F/F_0 \) within the peri-movement epoch were compared – traces were smoothed with a 40 point loess filter. Data were split based on their decoding accuracy scores and the bootstrapped median difference between high decoding accuracy neurons and those of the population were subtracted and a median difference calculated per sample. This process was repeated 10,000 times to generate a distribution for high decoding neurons versus the entire population and the same sampling procedure was used to investigate the correlations within low decoding accuracy neurons. To investigate spatial clustering, bootstrapped median differences between high decoding accuracy neurons and the population using pairwise distances (defined as the Euclidean distance between the centroids of manually drawn ROIs from 2-photon imaging processing) were compared. A Generalised Linear Mixed-Effects Model:

\[
    r \sim \text{distance}_{\text{pairwise}} \times \text{accuracy}_{\text{decoder}} + \text{action}_{\text{type}} + \text{animal}
\]

was used to model the pairwise correlation coefficient as a function of pairwise distance (continuous), decoding accuracy and action type. Pairwise distance and decoding accuracy were modelled as interacting fixed terms, while action type and animal were modelled as random intercepts to account for the dependency of the measurements on observations from the same animal and across the different action types. The model was estimated using the restricted maximum likelihood, or REML, method (Bartlett and Fowler, 1937). Model assumptions were verified by comparing residual versus fitted values for each covariate in the model against each covariate removed from the model.

**Statistics**
Data analysis was performed using custom-written scripts in MATLAB 2019a or Python v3.7. Data are reported as mean ± 95% bootstrapped confidence interval (10,000 bootstrap samples) unless otherwise indicated. Where multiple measurements were made from a single animal, suitable weights were used to evaluate summary population statistics. Statistical significance was considered when P<0.05 unless otherwise stated. Data were tested for normality and parametric/non-parametric tests were used as appropriate and as detailed in the text. The GLMM was designed in Python using the statsmodels library (Seabold and Perktold, 2010).

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Table of results

\( \bar{x} = \text{mean} \quad \tilde{x} = \text{median} \quad SD = \text{standard deviation} \quad \text{IQR} = \text{interquartile range} \)

\( \text{abd.} = \text{abduction} \quad \text{add.} = \text{adduction} \quad \text{fov} = \text{fields-of-view} \quad H / LDA = \text{high} / \text{low decoding accuracy} \quad \text{AB} = \text{action bias} \)

\( \text{GLMM} = \text{generalised linear mixed-effects model} \)

| Figure | Description | Sample size | Result | Variance | Confidence intervals (95%) | Statistical test result |
|--------|-------------|-------------|--------|----------|-----------------------------|------------------------|
| 1D-F   | Training time (days) | N = 12 | \( \bar{x} = 12.8 \) | SD = 2.6 | [11.3 14.2] | |
| 1E     | Successful trials / session (abd. / add.) | N = 12 | \( \bar{x} = 41.3 / 42.3 \) | SD = 7.2 / 7.2 | [37.5 45.2] / [38.4 45.9] | |
| 1F     | Vigour (ms; abd. / add.) | N = 12 | \( \bar{x} = 713.5 / 566 \) | SD = 7.2 / 7.2 | [706.5 733.5] / [537.25 573] | |
| 1H     | Norm. task success (%; abd. saline) | N = 6 | \( \bar{x} = 0.99 / 1.19 \) / 1.47 | SD = 0.49 / 0.79 / 0.65 | [0.66 1.31] / [0.67 1.74] / [1.04 1.93] | \( F(1,2) = 2.25, P = 1.4 \times 10^{-2} / 2.8 \times 10^{-2} / 0.3 \) |
|        | Norm. task success (%; abd. muscimol) | N = 6 | \( \bar{x} = 0.34 / 0.25 \) / 1.52 | SD = 0.19 / 0.14 / 0.60 | [0.22 0.47] / [0.15 0.34] / [1.11 1.96] | |
|        | Norm. task success (%; add. saline) | N = 6 | \( \bar{x} = 0.81 / 0.88 \) / 0.99 | SD = 0.09 / 0.26 / 0.40 | [0.76-0.88] / [0.68 1.03] / [0.76 1.28] | \( F(1,2) = 1.62, P = 3.2 \times 10^{-3} / 2.7 \times 10^{-2} / 0.9 \) |
|        | Norm. task success (%; add. muscimol) | N = 6 | \( \bar{x} = 0.35 / 0.48 \) / 0.98 | SD = 0.24 / 0.31 / 0.41 | [0.20 0.53] / [0.28 0.69] / [0.74 1.28] | |
| Supp.  | Neurons / 100 µm² (NeuN / GCaMP6s) | N = 1 / 7 | \( \bar{x} = 15.6 / 13.3 \) | SD = 0.9 / 2.7 | t(16) = 1.75, \( P = 0.2 \) | |
| 1C     | Prop. of responsive neurons (non / movement / reward) | N = 6 | \( \bar{x} = 20.9 / 73.5 \) / 5.7 | SD = 15.1 / 16.0 / 3.7 | [12.8 29.1] / [64.7 81.8] / [3.7 7.7] | |
|   | Description                                                                                                | N | fov | cell | Mean | IQR          | W | Z      | P     |
|---|-----------------------------------------------------------------------------------------------------------|----|-----|------|------|--------------|---|--------|-------|
| 2F| Prop. of movement-responsive neurons (non / abd. / add.)                                                  | N = 6 | fov = 12 | cell = 468 | $\bar{x} = 59.8 / 14.3 / 11.8$ | IQR = [42.9 74.3] / [12.7 28.6] / [8.2 27.7] |
|   | Supp. 2A: Action bias cell types (%; I-VI)                                                              | N = 6 | fov = 12 | cell = 181 | 75(136) / 10(19) / 7(12) / 4(7) / 3(5) / 1(2) |             |        |       |
|   | Supp. 2C: Prop. of biased neurons (equal / unequal baseline)                                           | N = 6 | fov = 12 | cell = 181 | $\bar{x} = 69.5 / 30.5$ | IQR = [63.2 71.4] / [28.6 36.8] |
| 2J| Prop. of biased neurons (highDA / lowDA)                                                                | N = 6 | fov = 12 | cell = 181 | $\bar{x} = 67.3 / 32.7$ | IQR = [42.6 79.3] / [20.7 57.4] |
| 2K| Prop. of movement-responsive neurons (LDA / HDA+AB / HDA-AB)                                           | N = 6 | fov = 12 | cell = 468 | $\bar{x} = 60.5 / 27.1 / 11.1$ | IQR = [34.7 78.1] / [11.8 51] / [5.7 14.3] |
| 3B| Decoding accuracy (single cell / population)                                                            | N = 6 | fov = 12 |             | $\bar{x} = 0.61 / 0.75$ | IQR = [0.58 0.65] / [0.63 0.79] | W = 1, Z = -2.20, P = 2.8x10^{-2} |
| 3F| Prop. neurons removed (high-low / random)                                                              | N = 6 | fov = 9  |             | $\bar{x} = 0.21 / 0.64$ | IQR = [0.11 0.61] / [0.41 0.98] | W = 1, Z = -2.20, P = 2.8x10^{-2} |
|   | Supp. 3A: Population decoding vs max $d'$                                                                | N = 6 | fov = 10 |             |             |             | r²=0.89, F(1,5) = 33.6, P = 4.3x10^{-3} |
| 3J| Prop. neurons removed (high-low / random)                                                              | N = 6 | fov = 10 |             | $\bar{x} = 0.15 / 0.35$ | IQR = [0.05 0.47] / [0.11 0.85] | W = 1, Z = -2.20, P = 3.1x10^{-2} |
| 4B| Norm. prop. $\Delta F/F_0$ onsets abduction (ms; HDA / LDA). ANOVA [animal:cell type: onset time]      | N = 6 | fov = 12 | cell = 468 | $\bar{x} = 119 / 85$ | IQR = [83.3 142.9] / [76.9 101.9] | F(5) = 0.43, P = 0.83 / F(1) = 0.19, P = 0.66 / F(12) = 5.83, P = 7.4x10^{-7} |
|   | Description | N = 6 | fov = 12 | cell = 468 | Mean $\bar{x}$ | IQR | F(5) = 0.43, P = 0.81 | F(1) = 0.19, P = 0.12 | F(12) = 5.83, P = 3.3x10^{-14} |
|---|-------------|-------|---------|----------|----------------|------|----------------------|---------------------|------------------------|
| 4C | Pairwise correlation coefficient (r; abduction; HDA vs ALL / LDA vs ALL) |       |         |          | $\bar{x}$ = -0.02 / 0.02 |      | [-0.22 0.14] / [-0.12 0.17] | $P = 0.85 / 1.0$ |
| 4D | Pairwise corr. Vs distance (HDA / LDA / ALL) |       |         |          | Spearman $r = -0.11 / -0.17 / -0.1$ |      | $P = 0.19 / 3.0x10^{-2} / 0.2$ |
|   | GLMM r distance pairwise accuracydecoder + actiontype+animal |       |         |          | $[-0.00 0.014] / [-0.00 0.00]$ |      | $P = 0.19 / 0.93$ |
| 4E | Pairwise distance (µm; HDA vs ALL / LDA vs ALL) |       |         |          | $\bar{x}$ = 3.9 / 1.7 |      | $[-38.5 52.2] / [-29.9 33.6]$ | $P = 1.1 / 1.0$ |
Supplementary Figures 1-4
Supplementary Figure 1. Population imaging in layer 5B of mouse primary motor cortex.

(A) Left, schematic showing mapped region of caudal forelimb area (CFA) centred on 0.6 mm anterior, 1.6 mm medial of bregma. Red cross denotes bregma. Right, heatmap indicating changes in layer 5B depth across a range of cortical coordinates. Values represent the mean depth in μm of the upper boundary of Layer 5B (N = 3 mice). (B) Left, representative image of NeuN stained layer 5B neurons. Right, two-photon image of L5B neurons expressing GCaMP6s. Small circles are regions of interest (yellow) drawn around individual neurons within a larger bounded area excluding blood vessels. (C) Average number of NeuN versus GCaMP6s expressing neurons / 100 μm² in layer 5B of CFA. Vertical bars depict standard error of the mean and grey dots represent individual slices (NeuN, n = 3 slices, N = 1 mouse; GCaMP6s, n = 15 slices, N = 7 mice; t(16) = 1.75, P = 0.2, two-sample t-test).
Supplementary Figure 2. Layer 5B neuronal response classification during abduction/adduction trials.

(A) Left, summary of layer 5B neuronal classification. Right, Proportion of cells displaying response types 1-6 and descriptive ∆F/F response profiles. (B) Representative action bias neurons with significant differences in intertrial baseline ∆F/F. Top, raster showing normalised ∆F/F across successive abduction or adduction trials. Bottom, ∆F/F, mean and 95% CI for abduction (purple) and adduction (blue) trials. Dashed lines represent onset of movement. (C) Proportion of action-biased neurons in layer 5B of caudal forelimb area with equal (black; median = 69.5, IQR [63.2 71.4]) and unequal (white; median = 30.5, IQR [28.6 36.8]) intertrial baseline ∆F/F0 for all 12 imaging fields-of-view (n = 181 neurons from 12 fields-of-view, N = 6 mice).
Supplementary Figure 3. A discrimination index for principal components of the population response.

(A) Relationship between population decoding accuracy and the maximum discrimination index (d’) (N = 6 mice, r² = 0.89, F(1,5) = 33.6, P = 4.3x10⁻⁵). Line denotes linear regression fit, with shaded region representing bootstrapped 95% CI. (B) Histogram of significant principal components (PCs) across all 12 fields-of-view (FOVs). (C) Relationship between the proportion of variance explained and the d’ for significant PCs across all 12 FOVs. PCs from different FOVs are colour-coded and joined with a line for ease of interpretation. Significant d’ values are distributed across the full range of PCs and there is no consistent relationship between d’ and variance explained.
Supplementary Figure 4. Layer 5B neuronal activity correlations during abduction/adduction trials.

(A) Functional networks of neuronal activity from the representative field-of-view (FOV) shown in Figure 4C during abduction and adduction trials. Line colour (light to dark) and width correspond to increasing values of Pearson’s r. Neurons are plotted as nodes in Euclidean space with colour (HDA - orange; LDA - grey) and size relating to increasing decoding accuracy (n = 468 neurons from 12 FOVs, N = 6 mice). (B) Box-and-whisker plots showing the median, interquartile range and range of correlation coefficients across mice for HDA (orange), LDA (grey) and all (brown) neurons during abduction (purple) and adduction (blue) trials.