Fabrication of Lensed Optical Fibers for Biosensing Probes Using CO\textsubscript{2} and Femtosecond Lasers

Ki-Dong Lim\textsuperscript{1,2,†}, Hun-Kook Choi\textsuperscript{2}, Ik-Bu Sohn\textsuperscript{2,3,*}, Byeong-Ha Lee\textsuperscript{3,*} and Jin-Tae Kim\textsuperscript{1,*}

\textsuperscript{1} Department of Photonic Engineering, Chosun University, Gwangju 61452, Korea; kdlim33@kopti.re.kr
\textsuperscript{2} Advanced Photonics Research Institute (APRI), Gwangju Institute of Science and Technology (GIST), Gwangju 61005, Korea; hunkook.choi@gist.ac.kr
\textsuperscript{3} School of Electrical Engineering and Computer Science, Gwangju Institute of Science and Technology (GIST), Gwangju 61005, Korea

* Correspondence: ibson@gist.ac.kr (I.-B.S.); leebh@gist.ac.kr (B.H.L.); kimjt@chosun.ac.kr (J.-T.K.);
Tel.: +82-62-230-7019 (J.-T.K.)

† Present address: Korea Photonics Technology Institute (KOPTI), Gwangju 61007, Korea.

Abstract: We propose a new method for precisely fabricating a lensed fiber with a desired focal length by first cleaving a coreless silica fiber using an ultrafast femtosecond laser without thermal effects and subsequently shaping the radius of curvature at the optical-fiber end using a CO\textsubscript{2} laser. The precisely cleaved segment of the coreless silica fiber obtained with the femtosecond laser is attached to a long single-mode fiber. The beam-exposure time and laser power of the CO\textsubscript{2} laser are adjusted to melt the coreless-fiber end to yield a uniform, consistent, and precise radius of curvature, thereby realizing a lensed optical fiber. The precision of the radius of curvature in this case is greater than those obtained with the conventional arc discharge method with thermal treatment requiring fairly complex processes and yielding relatively low fabrication accuracy. In our study, we observe a difference between the measured and calculated focal lengths of the fabricated lens, possibly because the exact value of the mode field diameter is uncertain. On the other hand, the beam size measured using the knife-edge method matches closely with the theoretical size. Our findings confirm the feasibility of fabricating lensed optical fibers for fiber-based biosensing using CO\textsubscript{2} and femtosecond lasers.

Keywords: CO\textsubscript{2} laser; femtosecond laser; lensed fiber; fiber cleaving

1. Introduction

Optical probes\textsuperscript{[1,2]} are widely used in optical coherence tomography (OCT) and other sensing and imaging systems for investigating the internal structures of biological tissues and the intraluminal imaging of various organs. However, conventional probes are bulky and unwieldy, and thus, researchers have considered replacing them with lensed optical fibers\textsuperscript{[3–5]}. In particular, a set of two lensed optical fibers can replace existing bulky optical lens systems for constructing compact microelectromechanical systems (MEMS) that can afford significantly improved imaging performances\textsuperscript{[6]}.

There are several conventional methods for fabricating the lensed optical fibers used in such compact MEMS setups. Current methods for introducing surface curvature at the optical-fiber tip include curing a photoreactive polymer with ultraviolet light\textsuperscript{[7]}, polishing the end tip of the fiber\textsuperscript{[8]}, melting the optical-fiber tail via arc discharge\textsuperscript{[6,9]}, and fusing a GRIN lens with the optical fiber\textsuperscript{[10]}.

Two of the abovementioned methods have found wide usage in the fabrication of lensed optical fibers. The first method involves fusing a GRIN lens with a gradually varying refractive index into an optical fiber, which requires very precise cleaving. In this method, a section of the GRIN lens is precisely cut off to focus a beam at the right position; however, the method requires precise calculations of the optical beam path within the
GRIN lens. The second method involves attaching a coreless silica fiber (CSF) to an optical fiber and using an arc discharge to shape the radius of curvature at the end of the CSF to form a lens [9]. With this approach, a beam from a lensed optical fiber can be made to converge or diverge depending on the CSF length and the radius of curvature of the CSF tip. This method also requires the precise cleaving of optical fibers to precisely adjust the CSF length. In addition to precise cleaving, it is also necessary to make the CSF end suitably curved. Thus, it is difficult to fabricate a lensed fiber using a CSF when compared with GRIN-lens-based fabrication. However, a specific focal length of the GRIN lens for a lensed optical fiber cannot be easily obtained for customized needs. Furthermore, precise cleaving is also necessary for using a GRIN lens when compared with the CSF-based method.

Against this backdrop, in this work, we apply a new method to fabricate lensed optical fibers with desired focal lengths by using femtosecond and CO$_2$ lasers. Here, the femtosecond laser is used to precisely cleave a CSF [11–13] directly without being heavily affected by thermal effects. We note that our precise CSF cleaving technique using a femtosecond laser has been implemented previously, demonstrating its superiority over conventional micromachining, which cannot be used to precisely fabricate an optical fiber [12]. Furthermore, the proposing method is simpler than the conventional method involving polishing processes together with thermal processing [14,15].

The CO$_2$ laser with a wavelength of 10.6 μm and having a suitable absorption rate for silicon material is used to melt the CSF tip to form the lens curvature. The method also yields a more uniform and consistent radius of curvature with a precision of ≤1 μm at the end of the optical fiber along with the desired focal length when compared with the widely used conventional arc discharge method [6,9]. The combination of cleaving a fiber and forming a lens on the optical-fiber tip described above provides a versatile approach to fabricate lensed optical fibers with precise focal lengths.

In our study, the focal length and size of the beam emerging from the manufactured lensed optical fibers are measured using a knife-edge method [16] and compared with the counterpart theoretical values. For calculation, we use the ABCD method for a Gaussian beam [17] to analyze beam propagation at the CSF section after beam divergence from the lead single-mode fiber (SMF) and focusing by the lensed fiber.

2. Ray Tracing Using Gaussian ABCD Matrix

Figure 1 shows the propagation of a beam through a lensed optical fiber composed of an SMF and a CSF section. The beam propagating through the SMF with a core diameter of 9 μm can be approximated as a Gaussian paraxial beam, and therefore, we can apply the ABCD matrix law with complex parameter q(z) to define the beam waist (ω) and the radius of wavefront curvature (R) [18] of the beam as a function of the axial distance z. Consequently, we can determine a focal length L, the distance from the end of the lens to the plane where the beam has a minimum beam waist (ω), as shown in Figure 1.

![Figure 1. Schematic of Gaussian-beam propagation through a lensed optical fiber.](image-url)
The evolution of the q-parameter can be calculated with the ABCD matrix, whose elements are given in matrix M. Parameter $q_2$ of the beam at the end of the SMF is related to the parameter $q_2$ at the focal plane as:

$$q_2 = \frac{Ad + B}{Cq_1 + D}$$

and

$$M = \begin{bmatrix} A & B \\ C & D \end{bmatrix}$$

where matrices $M_{01}$, $M_{12}$, $M_{23}$, and $M_{34}$ track the ray paths as per the paraxial optical approximation. Here, each of the matrices was calculated as $[19,20]$

$$M_{01} = \begin{bmatrix} 1 & 0 \\ \frac{n_1}{n_0} & 1 \end{bmatrix}, \quad M_{12} = \begin{bmatrix} 1 & L_C \\ 0 & 1 \end{bmatrix}, \quad M_{23} = \begin{bmatrix} \frac{n_2-n_1}{n_2R} & 0 \\ n_2 & 1 \end{bmatrix}, \quad M_{34} = \begin{bmatrix} 1 & L_f \\ 0 & 1 \end{bmatrix}$$

Here, $M_{01}$ denotes the ray matrix of the beam diverging from the boundary between the SMF and CSF, with $n_0 = n_1$. Moreover, $M_{12}$ describes the propagation of the beam through the CSF along geometrical path $L_C$ instead of optical path $nL_C$, which is the length $L_C$ between the exits of the SMF and the CSF in the case of the paraxial approximation. In addition, $M_{23}$ describes the path of the ray refracted by the lens and $M_{34}$ the ray path from the curvature of the lensed optical fiber with focal length $L_f$, with $n_1$ being the refractive index of the optical fiber of the CSF and $n_2$ the refractive index of air.

At the focal plane, because the Gaussian beam has an infinite radius of curvature there, we can calculate $L_f$ and $\omega_2$ as a function of $R$ and $L_C$:

$$L_f = \frac{-\alpha - a^2(\alpha L_C^2 + \beta L_C)}{\alpha^2 + a^2(\alpha L_C^2 + 2\alpha \beta L_C + \beta^2)}$$

and

$$\omega_2 = \omega_1 \sqrt{\frac{n_1}{n_2}},$$

where $a = -\frac{1}{\pi R} \frac{\lambda}{n_1 n_0 \omega_0^2}$, $\alpha = \frac{n_2-n_1}{n_2R}$ and $\beta = \frac{n_1}{n_2}$.

Figure 2 shows the behavior of $L_f$ calculated as functions of $R$ and $L_C$; the figure was generated using MATLAB. Here, $\lambda$ denotes the operating wavelength of 1550 nm and $\omega_1 = 5.2 \, \mu m$, which is half the mode field diameter (MFD) of the SMF. We use the MFD because the actual Gaussian beam size can be obtained from the size of the beam emerging partially from of the cladding of the SMF, and this beam is ~1 $\mu m$ larger than the actual core size [21].

![Forward focal length (μm)](chart.png)

**Figure 2.** Design of lensed optical fiber with desired focal length. The blue and dark yellow regions correspond to lensed optical fibers with long and short focal lengths, respectively.
From Figure 2, we can estimate that the R value must lie between ~70 \( \mu m \) and 120 \( \mu m \) and the \( L_C \) value must lie between ~275 \( \mu m \) and 400 \( \mu m \) to obtain the desired focal length of 375 \( \mu m \) (as indicated by the thick red contour line). The yellow region inside the red contour line in Figure 2 shows the \( L_C \) and R regime required for converging focal lengths instead of diverging negative focal lengths.

3. Experimental Methods

Figure 3 shows the procedure to fabricate an optical fiber integrated with a lens: (1) the SMF and CSF are fused by using an optical fiber fusion splicer, followed by (2) CSF cleaving using a femtosecond laser. Subsequently, the lens curvature is formed by (3) melting the clipped CSF tip using a \( CO_2 \) laser.

3.1. CSF Cleavage Using a Femtosecond Laser

To cleave the CSF precisely, we used a light-conversion Yb:KGW diode-pumped femtosecond laser (Model: Pharos) with a pulse repetition rate of 10–200 kHz, center wavelength of 1030 nm, pulse width of 250 fs, and maximum output of 6 W. The micromachining system consisted of X-and Y-axis linear motors with a moving range of 300 mm \( \times \) 300 mm and a maximum feeding rate of 300 mm/s. The resolution of the X- and Y-axes of the stage was 20 nm/count; we note here that the accuracy of the optical-fiber cleaving length of the CSF when using a femtosecond laser is governed by the resolution of the moving stage.

CSF cleavage was performed with the use of a jig with two holders to grip the CSF. One of the holders was moveable, and tension was applied along one direction. The femtosecond laser was operated at a repetition rate of 10 kHz and an output power of 23 mW. The processing speed was 0.1 mm/s, and line processing was performed once. The cleavage measurement of the CSF cut to a design length of 300 \( \mu m \) resulted in an actual length of 300.4 \( \mu m \), corresponding to a cutting precision of \( \leq 1 \mu m \).

3.2. Formation of the Radius of Curvature Using a \( CO_2 \) Laser

To shape the tip of the CSF into a curved surface, we varied the beam-exposure time and laser power of a coherent \( CO_2 \) laser (Model name: Diamond C-55L) having a central wavelength of 10.6 \( \mu m \) and a maximum output of 55 W. The beam was defocused a little to make the beam size larger than the tip size of the CSF using an object lens with the focal length of 25 mm. The machining range along the X and Y axes of the \( CO_2 \) laser processing system was 300 mm \( \times \) 300 mm, with an accuracy of 1 \( \mu m \). The maximum movement range of the Z-axis stage was 150 mm, with an accuracy of 1 \( \mu m \). To form the curvature of the CSF
tip, the optical fiber was placed parallel to the direction of the CO\textsubscript{2} laser beam using a CCD and moved with the use of XY and Z stages such that the fiber was located a little away from the focal plane of the CO\textsubscript{2} laser beam. A jig was used to fix and adjust the inclination of the optical fiber.

3.3. Measurement of Focal Length and Beam Size

Figure 4 shows the scheme used to measure the focal length and size of the beam emitting from the fabricated lensed optical fiber. Here, we used a laser light source with the operating wavelength of the SMF, i.e., 1550 nm. Because the tip of the circulator shown in Figure 4 was the APC-type, an APC-type ferrule was connected to the lensed optical fiber. In this setup, the laser beam with a wavelength of 1550 nm passes through the circulator, is made incident on the lensed optical fiber, and is reflected from the Au-coated mirror with good reflectance across all wavelength bands. The reflected beam again converges at the lensed optical fiber, and the beam travels to the laser power meter through the circulating device. In the study, the gold-coated mirror was moved in steps of 1 \( \mu \)m, and the change in the output power with respect to the mirror distance was measured using a laser-power measuring device. The mirror position at which the strongest output power was obtained as per the power meter was determined as the focal point of the lensed optical fiber.

![Figure 4. Cont.](image-url)
4. Experimental Results and Discussions

4.1. Measurement of the Radius of the Curvature of the Lensed Optical Fiber

Figure 5 shows the microscopic images of the lens fabricated using the CO$_2$ laser as a function of the exposure time. Spherical shapes are formed at the ends of the optical fibers instead of ellipsoidal shapes owing to internal material cohesion resulting from the melting of the optical fiber tips in the region where the lens curvature is shaped as a function of the CO$_2$ laser exposure time. The circular cross-section of the sphere was confirmed by comparing the formed circular perimeter with the perimeter drawn using the calculated radius of curvature.

The mirror was also moved laterally by 1 μm, and the output of the beam was measured. Figure 4c shows the method for measuring the Gaussian-beam profile using the knife-edge method. The method measures only a part of the laser power, except that of the Gaussian beam blocked by the knife edge, as a function of lateral mirror-position variation [18]. Thus, the Gaussian beam profile can be obtained from the laser-power gradient. The $1/e^2$ points of the obtained line profile can be obtained using these beam profiles, and consequently, the beam size can be determined.
Figure 5. Fabricated radii of curvatures of the optical fibers, with $P = 0.5 \text{ W}$ and the exposure times set to (a) 1 s, (b) 2 s, and (c) 3 s.

Figure 6 illustrates the method for measuring the radius of curvature of the fabricated lensed optical fiber. Three different points ($P_1$, $P_2$, and $P_3$) on the formed circular perimeter, including the vertex ($P_2$) of the formed sphere, are chosen as shown. Two different line segments ($P_2P_1$ and $P_2P_3$) are drawn from the vertex ($P_2$) of the sphere. Additionally, two bisectors, $a'$ and $b'$, are drawn perpendicular to line segments $a$ and $b$, respectively, which meet at the center of the circle, coinciding with the central coordinates of the sphere.

Figure 6. Measurement of the radius of curvature of the coreless silica fiber.
4.2. Measurement of the Focal Length and Beam Size

The mirror reflection method and the knife-edge method [14] were used to measure the focal length of the fabricated lensed optical fiber and the beam size at the focal plane, respectively.

The dimensions of the lensed fiber used for these measurements were $L_C = 308 \, \mu m$ and $R = 72.8 \, \mu m$ in Figure 5b. Here, we note that the $L_C$ value immediately after cleaving with the femtosecond laser was measured to be $300.4 \, \mu m$. However, after lens formation with the CO$_2$ laser, the $L_C$ value increased to $308 \, \mu m$, with a length increase of ~7 to 8 $\mu m$. Figure 7a shows the measurement results of the focal length of the fabricated lensed optical fiber. The intensity of the beam reflected by the mirror and returned to the lensed optical fiber was measured in terms of the mirror distance from the fiber tip. From the figure, we note that the largest intensity corresponds to a mirror distance of $375 \, \mu m$, that is, the focal length of the lensed optical fiber. Figure 7b shows the measurement of the beam size. By moving a sharp knife edge transversely in steps of $1 \, \mu m$ across the focal plane, we measured the intensity of the beam reflected by the knife edge in terms of the edge position. The figure shows the measured data (dotted black line), their fitting with a Boltzmann curve, and the differentiated curve denoted by the solid blue line. The knife edge was moved to reflect light from the mirror whenever the mirror position was changed by $1 \, \mu m$. From the measurement of the $1/e^2$ value of the intensity profile (blue line), we measured the beam size as $27 \, \mu m$.

Figure 7. Measurements of (a) focal length and (b) beam size of the lensed optical fiber.
4.3. Calculation of Focal Length and Beam Size

The measured focal length of the sample fiber with $L_C = 308 \, \mu m$ and $R = 72.8 \, \mu m$ was 375 $\mu m$; on the other hand, the theoretical focal length was 406 $\mu m$, corresponding to a difference of 31 $\mu m$. This difference between the measured and calculated focal lengths may be due to the uncertainty in the MFD of the SMF. The MFD of the SMF-28 communication optical fiber (Corning Corp.) used in this study was $10.4 \pm 0.5 \, \mu m$. Figure 8 shows the graph obtained by substituting the values of the nearby MFDs within the error range. We note that as the MFD value decreases by 0.1 $\mu m$, the focal length is sensitively changed by 10 $\mu m$. The red dotted line in Figure 8 indicates the focal length obtained by substituting the average MFD value of 5.2 $\mu m$ to obtain the theoretical focal length. We note here that the error further depends on the optical-alignment conditions.

![Figure 8. Variation in the focal length as a function of the MFD size.](image)

The beam size for the focal length of 406 $\mu m$ was also measured using the knife-edge method, and it was estimated as 27 $\mu m$ at $1/e^2$ of the peak intensity. When compared with the theoretical beam size of 23 $\mu m$ at the $2\omega_z$ point, the error was 4 $\mu m$.

5. Conclusions

We propose and demonstrate a new method for fabricating precisely a lensed fiber with a desired focal length by cleaving a CSF using an ultrafast femtosecond laser without appreciable thermal effects and forming the radius of curvature at the end of this optical fiber using a CO$_2$ laser. In our study, a precisely cleaved segment of a CSF was obtained using a femtosecond laser and the segment was attached to a long SMF. The CO$_2$ laser was used to melt the end of the coreless fiber to precisely shape the radius of curvature with a precision of $\leq 1 \, \mu m$ as a function of the exposure time and the power of the CO$_2$ laser beam, thereby resulting in a focal length as close as possible to the design value using simulated parameters in Figure 2. This technique forms an alternative to other conventional methods for forming fiber lenses for biosensing applications. The method can be used to realize a broad range of focal lengths with variable CSF lengths and curvature radii of the lenses for application to various imaging requirements.

In the study, we used a CO$_2$ laser to fabricate a lensed optical fiber with $L_C = 308 \, \mu m$ and $R = 72.8 \, \mu m$ at the end of the CSF. The simulated and calculated focal lengths were compared with the actually measured focal length. Furthermore, the MFD of the SMF-28 communication optical fiber was varied from 9.9 $\mu m$ to 10.9 $\mu m$, and the obtained focal length of 406 $\mu m$ with the mean MFD differed from the designed and theoretical focal distance of 375 $\mu m$. This difference between the measured and the calculated focal lengths can be attributed to the uncertainty associated with the MFD.
The beam size at the focal length of 406 µm was also measured using the knife-edge method, and it was estimated as 27 µm at 1/e² of the peak intensity. The theoretical beam size was 23 µm at the 2ω₀ point, corresponding to an error of 4 µm with respect to the experimental value. These findings indicate that it is possible to fabricate a lensed optical fiber with a desired focal length by using femtosecond and CO₂ lasers. Furthermore, lenses with optimum converging and diverging focal lengths can be obtained by varying L and R for diverging or converging the light. Therefore, these lenses can be used as fine optical elements in OCT or MEMS.

In the study, we applied the paraxial approximation based on the ABCD matrix to trace the focal point; however, in future, it would be worthwhile to confirm the difference between the measured and the calculated focal lengths with general approaches using ray-tracing methods. We also plan to examine the systematic statistical repeatability and precision of fabricated micro-lenses using a large number of fabricated samples to determine the shortest range of focal lengths possible with the method.

Author Contributions: Conceptualization, K.-D.L., I.-B.S. and J.-T.K.; methodology, K.-D.L., H.-K.C., I.-B.S. and J.-T.K.; software, K.-D.L. and J.-T.K.; validation, I.-B.S., B.-H.L. and J.-T.K.; formal analysis, K.-D.L. and J.-T.K.; investigation, K.-D.L. and J.-T.K.; writing—original draft preparation, J.-T.K.; writing—review and editing, B.-H.L. and J.-T.K.; visualization, I.-B.S. and J.-T.K.; project administration, I.-B.S. and J.-T.K. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Institutional Review Board Statement: Not applicable.

Informed Consent Statement: Not applicable.

Data Availability Statement: Not applicable.

Acknowledgments: The authors are grateful to Soongho Park (National Institutes of Health, USA) for providing valuable comments toward improving the original manuscript. This work was supported by a research fund from Chosun University (2019).

Conflicts of Interest: The authors declare no conflict of interest.

References
1. Fujimoto, J.G.; Pitris, C.; Boppart, S.A.; Brezinski, M.E. Optical coherence tomography: An emerging technology for biomedical imaging and optical biopsy. Nat. Neoplasia 2000, 2, 9–25. [CrossRef] [PubMed]
2. Huang, D.; Swanson, E.A.; Lin, C.P.; Schuman, J.S.; Stinson, W.G.; Chang, W.; Hee, M.R.; Flotte, T.; Gregory, K.; Puliafito, C.A.; et al. Optical coherence tomography. Science 1991, 254, 1178–1181. [CrossRef]
3. Lee, B.H.; Min, E.J.; Kim, Y.H. Fiber-based optical coherence tomography for biomedical imaging sensing, and precision measurements. Opt. Fiber Technol. 2013, 19, 729–740. [CrossRef]
4. Park, S.; Rim, S.; Kim, J.W.; Park, J.; Sohn, I.-B.; Lee, B.H. Analysis of design and fabrication parameters for lensed optical fibers as pertinent probes for sensing and imaging. Sensors 2018, 18, 4150. [CrossRef] [PubMed]
5. Ryu, S.Y.; Choi, H.Y.; Na, J.H.; Choi, W.J.; Lee, B.H. Lensed fiber probes designed as an alternative to bulk probes in optical coherence tomography. Appl. Opt. 2008, 47, 1510–1516. [CrossRef] [PubMed]
6. Wu, G.; Mirza, A.R.; Gamage, S.K.; Ukrainczyk, L.; Shashidhar, N.; Wruk, G.; Ruda, M. Design and use of compact lensed fibers for low cost packaging of optical MEMS components. J. Micromechanics Microengineering 2004, 14, 1367–1375. [CrossRef]
7. Kim, K.-R.; Chang, S.; Oh, K. Refractive microlens on fiber using UV-curable fluorinated acrylate polymer by sur-face-tension. IEEE Photonics Technol. Lett. 2003, 15, 1100–1102.
8. Tseng, Y.; Huang, J.; Su, W. Fabricating lensed fiber using a novel polishing method. J. Manuf. Sci. Eng. 2009, 131, 041016. [CrossRef]
9. Qiu, Y.; Wang, Y.; Belfield, K.D.; Liu, X. Ultrathin lensed fiber-optic probe for optical coherence tomography. Biomed. Opt. Express 2016, 7, 2154–2162. [CrossRef]
10. Wang, C.; Sun, J.; Sun, F.; Zhu, J.; Yuan, Z.; Asundi, A. Coupling efficiency of ultra-small gradient-index fiber probe. Opt. Commun. 2017, 389, 265–269. [CrossRef]
11. Shah, L.; Tawney, J.; Richardson, M.; Richardson, K. Femtosecond laser deep hole drilling of silicate glasses in air. Appl. Surf. Sci. 2001, 183, 151–164. [CrossRef]
12. Lim, K.D.; Choi, H.-K.; Kim, J.T.; Lee, J.K.; Sohn, I.-B. Precision cutting and cleaving of optical fiber with femtosecond and CO₂ Laser. J. Korean Soc. Precis. Eng. 2017, 34, 633–637. [CrossRef]
13. Wang, Y.; Liao, C.R.; Wang, D.N. Femtosecond laser-assisted selective infiltration of microstructured optical fibers. Opt. Express 2010, 18, 18056–18060. [CrossRef] [PubMed]

14. Boyd, K.; Rees, S.; Simakov, N.; Daniel, J.M.O.; Swain, R.; Mies, E.; Hemmings, A.; Clarkson, W.A.; Haub, J. High precision 9.6 μm CO₂ laser end-face processing of optical fibers. Opt. Express 2015, 23, 15065–15071. [CrossRef]

15. Le’vesque, L.; Jdanov, V. Optical fiber cleaved at an angle by CO₂ laser ablation: Application to micromachining. Opt. Laser Technol. 2010, 42, 1080–1083. [CrossRef]

16. Suzaki, Y.; Tachibana, A. Measurement of the μm sized radius of Gaussian laser beam using the scanning knife-edge. Appl. Opt. 1975, 14, 2809–2810. [CrossRef]

17. Kogelnik, H.; Li, T. Laser beams and resonators. Appl. Opt. 1966, 5, 1550–1567. [CrossRef]

18. Kogelnik, H. On the propagation of Gaussian beams of light through lenslike media including those with a loss or gain variation. Appl. Opt. 1965, 4, 1562–1569. [CrossRef]

19. Emkey, W.L.; Jack, U.A. Analysis and evaluation of graded-index fiber-lenses. J. Light Wave Technol. 1987, 5, 1156–1164. [CrossRef]

20. Kishimoto, R.; Koyama, M. Coupling characteristics between single-mode fiber and square law medium. IEEE Trans. Microw. Theory Tech. 1982, 30, 882–893. [CrossRef]

21. Artiglia, M.; Coppa, G.; Vita, P.D.I.; Potenza, M.; Sharma, A. Mode field diameter measurements in single-mode optical fibers. J. Light Wave Technol. 1989, 7, 1139–1152. [CrossRef]