LEARNING IMAGE LABELS ON-THE-FLY
FOR TRAINING ROBUST CLASSIFICATION MODELS

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ABSTRACT

Current deep learning paradigms largely benefit from the tremendous amount of annotated data. However, the quality of the annotations often varies among labelers. Multi-observer studies have been conducted to study these annotation variances (by labeling the same data for multiple times) and its effects on critical applications like medical image analysis. This process indeed adds extra burden to the already tedious annotation work that usually requires professional training and expertise in the specific domains. On the other hand, automated annotation methods based on NLP algorithms have recently shown promise as a reasonable alternative, relying on the existing diagnostic reports of those images that are widely available in the clinical system. Compared to human labelers, different algorithms provide labels with varying qualities that are even noisier. In this paper, we show how noisy annotations (e.g., from different algorithm-based labelers) can be utilized together and mutually benefit the learning of classification tasks. Specifically, the concept of attention-on-label is introduced to sample better label sets on-the-fly as the training data. A meta-training based label-sampling module is designed to attend the labels that benefit the model learning the most through additional back-propagation processes. We apply the attention-on-label scheme on the classification task of a synthetic noisy CIFAR-10 dataset to prove the concept, and then demonstrate superior results (3-5% increase on average in multiple disease classification AUCs) on the chest x-ray images from a hospital-scale dataset (MIMIC-CXR) and hand-labeled dataset (OpenI) in comparison to regular training paradigms.

1 INTRODUCTION

Supervised deep learning methods, although proven to be effective on many tasks, rely heavily on the quality of the data and its corresponding annotations. Some tasks enjoy almost error-free annotation, such as handwritten numbers and simple natural images. However, for other applications including most medical image analysis tasks, the inherent ambiguity of the task leads to unavoidable noise and fuzziness within the annotations themselves, no matter how experienced the expert labelers are. Meanwhile, under a multi-labeler setting for quality control purpose, the significant intra- and inter-observer variability injects even more uncertainties into the resulting labels. Beyond the above challenges, for the specific task of chest X-ray image classification, due to the fact that most labels of the available large-scale open datasets are automatically mined by Natural Language Processing (NLP) algorithms, there will be yet another layer of error-prone operation on top of existing variability. Ideally, we would prefer multiple manually and reliably labelled close-to-truth annotations, while in reality, most of the data only have a single annotation from an algorithm with relatively low accuracy.

Learning to learn from a variety of data (labels) falls within the scope of meta-learning, which is popular in many machine learning application, e.g., domain adaptation/generalization [Finn et al., 2017] [Dou et al., 2019] and few-shot learning [Snell et al., 2017] [Liu et al., 2019]. Those previous meta-learner models (as illustrated in Fig. 1(b)) often focus on learning the distribution of data (inputs of tasks) and specifying the update strategy of learner model parameters. Indeed, data from different sets (distributions) will contribute to the final learner model. On the contrary, we do not want the model to learn from erroneous labels (from less-experienced labelers) but learn only from “true” labels. We utilize the learner model parameters (via a meta-training process) to sample “true” labels for training a single learner model (as shown in Fig. 1(c)).
Figure 1: The diagram shows the difference of three learning paradigms in terms of how gradients are utilized for the training, i.e., (a) regular gradient based learning; (b) Meta-learning with multiple learning targets; (c) Proposed: learning the weights of each label \((y_a, y_b, y_c)\) in meta-training and then computing the weighted summation \(\hat{y}\) of labels for computing the final loss with prediction \(\hat{y}\).

To address these challenges, we proposed an attention-on-label strategy to benefit the training from multiple labels on the same subject. Instead of the resource-demanding process of asking several human annotators to label the same data, we choose to utilize annotations from different algorithm-based labelers, which only add little overhead beyond the single-labeler scenario. A meta-training scheme is adopted and integrated in our proposed label-sampling module to attend the labels that benefit the model learning the most through additional back-propagation processes.

Our contributions in this work are three-fold: 1) We proposed a training framework to compute the image labels on-the-fly in the classification tasks. A meta-training based approach is introduced to attend and sample the labels from multiple annotators; 2) Gradient flows towards the label are investigated and implemented. Indeed, the multiple sets of labels are inputs to the training framework. Learnable operations of the labels will require additional updates of label-related parameters; 3) We not only prove the concept on CIFAR-10 but also perform experiments on two chest X-ray datasets with both image-only and image-text classification tasks. In all datasets, superior performance of the proposed method is demonstrated in the image classification tasks compared to baseline methods.

2 RELATED WORKS

Meta learning: Meta learning aims to learn a generalizable model by situating itself at a higher level than conventional learning. This can be achieved in several ways such as finding weights that can be easily adapted to other models (Finn et al., 2017) or domains (Li et al., 2018a) during the training process. Meta learning results in models that can converge quickly with a few examples (Ravi & Larochelle, 2017). They all share a similar meta-training process while the various goals of meta-training can divide them to different routes as examples shown in Fig. 1. In this work, we target at weighting the importance of each label set based on its meta-training feedback and learning from the most effective labels.

Learning from noisy labels: Learning from noisy labels (Natarajan et al., 2013; Li et al., 2020; Zhang et al., 2020b) has been a popular topic in deep learning due to its prevalence in many existing datasets with intra- and inter-observer variability, and the inherent uncertainties of both data and task themselves. For medical imaging applications with a high degree of ambiguity, this issue is even more significant. Recent works attempt to address this challenge via a consistency loss with a teacher model (Li et al., 2019), loss weighting with 2nd order derivatives (Zhang et al., 2020b), and for medical image specifically, an online uncertainty sample mining strategy (Xue et al., 2019). Please note that they all focus on noise labels from a single annotator, while we attempt to use an attention mechanism to utilize labels from different sources together.

Multi-label classification in chest X-ray: Because of its wide application and easy accessibility, chest X-ray is one of the major research areas in the field of medical image analysis. Among the pioneering works (Wang et al., 2017; Rajpurkar et al., 2017; Yao et al., 2017; Li et al., 2018b; Tang et al., 2018; Chen et al., 2018; Hwang et al., 2019) in this area of deep learning, TieNet (Wang et al., 2018) first introduces an end-to-end trainable CNN-RNN architecture to extract distinctive text representations in addition to image features for improving label quality. More recently, a graph model was incorporated to enhance the learning accuracy (Zhang et al., 2020a).

Multi-observer studies: To ensure the annotation quality, especially for medical images where high expertise is required, it is common to have multiple annotations performed on the same set of data
Table 1: Uncertainties (_u) and positives (_p) of 6 sample disease findings from two labelers.

| label sets    | aletctasis | cardiomegaly | consolidation | edema | pneumonia | pneumothorax |
|---------------|------------|--------------|---------------|-------|-----------|--------------|
| negbio_u      | 10986      | 11899        | 3348          | 13204 | 19029     | 1112         |
| negbio_p      | 47804      | 40509        | 11088         | 27911 | 16122     | 9885         |
| u/p ratio     | 0.229      | 0.293        | 0.301         | 0.473 | 1.18      | 0.112        |
| chexpert_u    | 10662      | 6235         | 4446          | 13817 | 18915     | 1177         |
| chexpert_p    | 47629      | 46373        | 11231         | 28339 | 16757     | 11046        |
| u/p ratio     | 0.223      | 0.134        | 0.395         | 0.487 | 1.128     | 0.106        |

Table 1: Uncertainties (_u) and positives (_p) of 6 sample disease findings from two labelers.
GAP layer is the necessity to pass concatenated image and text features to a fully-connected layer for the final classification.

We adopt the most common loss functions for the multi-label classification prediction \( \hat{y} \), i.e., binary cross entropy (BCE) loss:

\[
L_{\text{C}}(\hat{y}, y) = -\frac{1}{N} \sum_{i=1}^{N} y_i \log \hat{y}_i + (1 - y_i) \log(1 - \hat{y}_i).
\]

Other more advanced losses could also be employed, while this type of improvement is out-of-scope in this paper. Here, we would like to demonstrate the feasibility and benefit of applying our proposed meta-training process with attention-on-label over a vanilla model. Other critical issues, like the unbalanced numbers of pathology comparing with “normal” classes, are not considered here either to keep the evaluation simple and effective.

3.2 ATTENTION ON LABELS

The overall training procedure is illustrated in Algorithm 1. For each training iteration, we input each data entry \((x, Y)\) from the training set and \(Y = \{y_1, \ldots, y_m, \ldots, y_M\}\) are \(M\) sets of image labels. During the meta-training, we compute the BCE loss \(L_{\text{C}}(\hat{y}, y_m, \theta)\) between the prediction \(\hat{y}\) of current classification model \(\theta\) and label set \(y_m\) and then perform the back-propagation to compute a new set of model parameters \(\hat{\theta}_m\),

\[
\hat{\theta}_m = \theta - \alpha \nabla_{\theta} L_{\text{C}}(\hat{y}, y_m, \theta),
\]

\(\alpha\) is the learning rate for this meta-training process. We then compute a set of new features \(\{F_m\}_{m \in \{1, \ldots, M\}}\) via the inference of image \(x\) using each meta-model \(\hat{\theta}_m\) individually. \(\{F_m\}\) could be either image features (i.e., output of the GAP) or one concatenated with text embedding (detailed in Section 3.3). \(\{F_m\}\) represent the feedback of model updates with each label set \(y_m\), i.e., the change that each \(y_m\) has brought to the model \(\theta\). Other types of feedback from each noisy label could also be utilized here, e.g., the gradients \(\{\nabla_{\theta} L_{\text{C}}(\hat{y}, y_m, \theta)\}_{m \in \{1, \ldots, M\}}\). Here, we take \(\{F_m\}\) as an example to compute the weight \(w_m\) for each label set via a softmax based attention mechanism,

\[
w_m = \text{softmax}(W_{\text{attn}}(\text{Cat}(\{F_m\}) + b_{\text{attn}}),
\]

where \(W_{\text{attn}}\) and \(b_{\text{attn}}\) are learnable parameters in our attention-on-label module. \(\text{softmax}\) is the activation function. \(\text{Cat}\) represents the concatenation as a stack of all features. \(w_m\) indicates the importance/correctness of label set \(y_m\) and is applied to compute the weighted average of all label sets for each data sample. Here, we employ a common softmax-based attention mechanism [Xu et al. 2015; Chen et al. 2017] as a sample case and many other more advanced learning-based attention mechanisms can be adopted to compute the weights, e.g., self-attention [Vaswani et al. 2017].
we embed the text report to a 768 dimension real-valued vector using the uncased version of BioBert. We update the model once more with the attended label and a global learning rate $\beta$ where $k$ is a threshold to slightly adjust the value range. Finally, we update the model once more with the attended label and a global learning rate $\beta$ for this iteration,\[
\hat{\theta} \leftarrow \theta - \beta \nabla L_C(\hat{y}, \tilde{y}, \theta). \tag{4}
\]

### Gradient Flows Towards Labels

Extra gradient flows (highlighted in red in Fig.2) are required for training our attention-on-label mechanism, specifically the parameters in Eq. 2. Most of the current learning frameworks have gradient flows (highlighted in green in Fig.2) with the images in the end since the labels are usually fixed or smoothed in advance (Müller et al., 2019). However, the gradients in our proposed framework not only flow to the images but also go through towards the labels since the final labels $\hat{y}$ are computed on-the-fly with learned weights/attentions. To our best knowledge, this concept of gradients towards labels is novel and has not been investigated and implemented before. Indeed, the inputs to the attention-on-label module are $M$ sets of labels and the computed features $\{F_m\}$, which are detached (without auto-computed gradients) and stacked during the meta-training. Therefore, additional parameter updating is required at the end of each iteration,\[
W_{attn} \leftarrow W_{attn} - \beta \nabla L_C(\hat{y}, \tilde{y}, W_{attn}), \quad b_{attn} \leftarrow b_{attn} - \beta \nabla L_C(\hat{y}, \tilde{y}, b_{attn}). \tag{5}
\]

### 3.3 Image-Text Embedding

Clinical textual material, e.g., clinical notes (Pelka et al., 2019) and radiology reports (Wang et al., 2018), contains richer information. We include the text report as an input to the classification problem to see if our proposed learning process will still benefit the learning and further improve the classification accuracy. There are a variety of approaches to generate text embedding, e.g., Fisher vectors of word2vec (Klein et al., 2015), bidirectional LSTMs (Wang et al., 2016), and the most recently developed BERT model (Devlin et al., 2018). To keep the simplicity of our baseline model, we embed the text report to a 768 dimension real-valued vector using the uncased version of BioBert (Lee et al., 2020), followed by two fully connected layers with 512 neurons each.

### 4 Experiments

#### 4.1 Datasets

**CIFAR-10**: We simulate 5 different types of annotators (with different experience) in a similar manner as Tanno et al. (2019) by injecting label noises into the training set of CIFAR-10, namely 1) hammer-spammer (HS), 2) structured-flips (SF), 3) ordered-confusion (OC), 4) Adversarial (AD), and 5) average (AVG) of 1-4. Each set of noisy labels are generated based on the defined confusion matrices for each type (as shown in Fig. 3). Whether each sample would have a noisy label is...
randomly selected while the overall noisy distribution should correspond to each confusion matrix, individually. Within all the noisy training data, we randomly select 20% as the validation set.

**MIMIC-CXR**: The MIMIC Chest X-ray ([Johnson et al., 2019](#)) database is a large publicly available dataset of chest radiographs with labels mined from image-associated text radiology reports using two different NLP based annotation tools, i.e., negbio ([Peng et al., 2018](#)) and chexpert ([Irvin et al., 2019](#)). The uncertain findings are marked as -1 in the original datasheet. Here, uncertainties are set to either 0 or 1 to form 4 different label sets, i.e., negbio_u0, negbio_u1, chexpert_u0, and chexpert_u1. The dataset contains 377,110 radiographs and labels from the 227,827 free-text radiology reports. Totally, 14 disease findings are listed \( (N = 14) \). In our experiments, only the frontal view images are adopted, the number of which is equal to the number of reports. We utilize the official data split for training, validation and testing. Following the same labeling protocol proposed by Demner-Fushman et al. ([2012](#)), we randomly selected 1000 images and associated textual reports from the testing set of MIMIC-CXR as the **MIMIC-CXR 1K hand-labeled Test** set. One of our staff (trained by a board-certified radiologist) hand-labeled the image by assigning the 14 labels manually to each image based on the reports.

**OpenI**: OpenI ([Demner-Fushman et al., 2015](#)) is a public dataset of chest X-rays collected from multiple institutes by Indiana University. In total, we fetch 3,851 unique radiology reports and 7,784 associated frontal/lateral images. To keep the consistency with MIMIC-CXR dataset, we use the same 14 categories of findings as mentioned above in the experiments. In our experiments, only 3,643 unique front view images and corresponding reports are evaluated.

### 4.2 Comparison Study:

The following methods in addition to the proposed method (**Ours**) are included in the comparison:

**ResNet-50** ([R50, He et al., 2016](#)): We take the network based on ResNet-50 as a baseline. It adopts an ImageNet pre-trained ResNet-50 (from Conv1 to Res5c) as the backbone, followed by a GAP layer and a fully-connect layer for the final classification. Optionally, BioBert embedded text features will be concatenated with the output of GAP before the classification.

**CM** ([Tanno et al., 2019](#)): This method multiplies a confusion matrix with the probability that the model produces for each class. The basic assumption is that this confusion matrix can correct the missed labeled data and return the probability for the truth using the learned confusion matrices. We carefully implement it according to the code snapshot provided by the authors.

**NG** ([Zhang et al., 2020a](#)): This method utilizes the prior knowledge of the disease relations as a form of knowledge graph. By injecting such prior knowledge and employing a graph convolutional network, it learns the underlying info for the final classification and report generation task. It is worthy to note that the results we report in the experiments are produced by a model that is both trained and evaluated on the OpenI dataset.

**TieNet** ([Wang et al., 2018](#)): It focuses more on how to learn the image and text embedding together using a CNN+RNN framework. Its LSTM based text embedding is relatively more complicated but also more representative through learning. We only adopt the text embedding from a pre-trained BioBERT model for our comparison, which is less customized.

**Evaluation Metric**: Receiver Operating Characteristic (ROC) curve is the standard metric to evaluate the performance of multi-label classification tasks. Here, Area Under the Curve (AUC) values
are computed for all the experiments on MIMIC-CXR and OpenI. We compute the multi-class classification accuracy (using sklearn.metrics.accuracy_score) for all the experiments on CIFAR-10.

4.2.1 IMPLEMENTATION DETAILS:

For pre-processing, we resize the image to 256×256 (while keeping the size of 32×32 for CIFAR-10) and normalize the image intensities to [0, 1]. No data augmentation is employed in our experiments. As mentioned above, we set the learning rate for the meta-training phase as $\alpha = 0.2$ and global learning rate as $\beta = 1e^{-4}$. The best model for all hyper-parameters are determined via validation. We set $k = 50$ and $T = 0.5$ empirically in the differentiable binarization module. We use a single NVIDIA Titan-X Pascal for training each classification model with a uniform batch size $B = 32$ across all the experiments. Adam optimizer is utilized for training all the compared models.

4.3 CLASSIFICATION RESULTS ON CIFAR-10

To prove the concept, we employ CIFAR-10 with 5 types of added noises in labels to illustrate that the proposed attention-on-label scheme can be beneficial for the model training using multiple noise label sets. Table 2 illustrates the multi-class classification accuracy on the CIFAR-10 testing set. Noise-levels are computed in (1-Accuracy) using corresponding confusion matrices. In general, better quality labels and data lead to better trained models. Noise introduced by structured flips confuse the model training more than other types. Here, HS represents a more experienced set of annotators and models trained with it obtained a high accuracy. A VG represents the results of learning from a label set with simple average of the noise-level (defined by the confusion matrices) of all annotators. Our proposed method achieves over 12% and 8% performance improvements over A VG and the previous state-of-the-art CM.

In addition, we also investigate how the label noise level and number of annotators will affect the model performance (detailed in Sec. A.2). With noise level ranged from 10% to 80%, Ours can constantly achieve better or similar results as the models trained with the relatively more accurate labels (e.g., AVG and HS). While experimenting with different number (2-5) of annotators, we observe a surge of the classification accuracy after including more than 2 annotators’ labels. Ours often out-performs CM while the number of annotators increase, especially when labels with high noise levels are employed.

4.4 CLASSIFICATION RESULTS ON CHEST X-RAY IMAGES

Classification Results Using Chest X-ray Images: Table 3 shows the evaluation results for all the compared method using only the images as the input to the model. The left side of Table 3 shows the AUCs of all the finding categories from R50, CM and ours. The averaged AUC for ours actually drops from the baseline. Considering the fact that the testing set of MIMIC-CXR dataset is also using the algorithm based labels, our predictions actually diverge from those noisy labels and lean to the underlying true labels. It is proved by the results illustrated in OpenI dataset section (right part of Table 3). OpenI dataset has the hand-labeled ground truth and our method is able to achieve over 4% increase in the averaged AUC, which is also greater than what the CM method achieves. Although, both NG and TieNet partially utilized the report textual information in their image classification framework, Ours still is able to obtain equivalent or better results in most of the detailed disease categories. As mentioned above, those disease categories with larger amount of uncertainties provide more information and therefore benefit more from the proposed meta-training process, e.g., Atelectasis and Consolidation. Please see the Appendix for more detailed results.

Classification Results Using Both Chest X-ray Images and Report Texts: We observe similar improvements on the image-text classification task. Indeed, the text report contains more information about the disease diagnosis (maybe more than the image itself). We also observe the increase of the
Table 3: Classification AUCs for 14 findings in Chest X-Rays using the testing set of MIMIC-CXR (with NLP generated labels) and OpenI dataset (hand-labeled GT). E-cardio: enlarged-cardiomiastium; Pneum-x: pneumothorax. More details in Table 6 of the Appendix.

| Disease          | MIMIC-CXR Test (NLP) | OpenI (hand-labeled) |
|------------------|----------------------|----------------------|
|                  | R50 | CM | ours | MG | TieNet | R50 | CM | ours |
| Atelectasis      | 0.821 | 0.832 | 0.826 | 0.833 | 0.774 | 0.781 | 0.81 | 0.826 |
| Cardio           | 0.825 | 0.852 | 0.879 | 0.913 | 0.847 | 0.859 | 0.881 | 0.879 |
| Consol.          | 0.762 | 0.751 | 0.906 | -    | -    | -    | 0.829 | 0.842 | 0.906 |
| Edema            | 0.887 | 0.903 | 0.885 | 0.931 | 0.879 | 0.895 | 0.924 | 0.885 |
| E-cardio         | 0.74  | 0.757 | 0.725 | -    | -    | 0.795 | 0.758 | 0.725 |
| Fracture         | 0.722 | 0.771 | 0.632 | 0.671 | -    | 0.513 | 0.596 | 0.632 |
| Lesion           | 0.765 | 0.744 | 0.643 | 0.643 | 0.658 | 0.585 | 0.58  | 0.643 |
| Opacity          | 0.814 | 0.82  | 0.775 | 0.803 | -    | 0.742 | 0.738 | 0.775 |
| No-finding       | 0.857 | 0.863 | 0.775 | 0.747 | 0.754 | 0.739 | 0.775 |
| Effusion         | 0.906 | 0.914 | 0.942 | 0.942 | 0.899 | 0.912 | 0.932 | 0.942 |
| Pleural-o.       | 0.866 | 0.829 | 0.705 | -    | -    | 0.648 | 0.676 | 0.705 |
| Pneumonia        | 0.809 | 0.809 | 0.871 | 0.863 | 0.731 | 0.781 | 0.823 | 0.871 |
| Pneum-x          | 0.866 | 0.858 | 0.833 | 0.843 | 0.709 | 0.793 | 0.882 | 0.833 |
| Devices          | 0.92  | 0.926 | 0.729 | 0.805 | -    | 0.628 | 0.655 | 0.729 |
| Average          | 0.858 | 0.851 | 0.794 | -    | -    | 0.783 | 0.774 | 0.794 |
| **Image only**   | 0.941 | 0.927 | 0.931 | -    | -    | 0.809 | 0.824 | 0.835 |

Table 4: Averaged classification AUCs for 14 findings using the MIMIC-CXR 1K hand-labeled Test set. negbio_u1, negbio_u0, chexpert_u1, and chexpert_u0 are derived from the original NLP mined labels by setting the uncertainty to either 1 or 0. See all diseases’ AUCs in the Appendix.

| AUC          | MIMIC-CXR 1K hand-labeled Test |
|--------------|---------------------------------|
|              | negbio_u1 | negbio_u0 | chexpert_u1 | chexpert_u0 | R50 | CM | Ours |
| **Average**  | 0.869     | 0.805     | 0.866       | 0.809       | 0.842 | 0.837 | 0.868 |

5 Conclusion and Final Remarks

In this paper, we introduced a novel learning framework (meta-training with the attention-on-label module) for handling data with multiple noisy label sets. The variability that the multiple label sets bring could in fact benefit the learning of a more accurate and robust model. We demonstrated the application of our proposed method on both multi-label and multi-class classification tasks and we believe it will be quite straight-forward to adapt it for other task, e.g., image segmentation. Indeed, the proposed method provides a viable way to handle the challenges of learning large-scale data with algorithm generated labels, where the label is a huge burden, especially for medical image analysis.

The proposed label sampling module convert the hard labels (0 or 1) to soft labels (a value between 0 and 1) and it also reduces the overfit towards erroneous labels, which is similar to the idea of label smoothing [Müller et al., 2019]. Different to hard label smoothing, we assigned the new label on-the-fly (based on the network feedback) instead of instantly replacing 0 and 1 with $0 + \epsilon$ and $1 - \epsilon$. Such setting is extremely effective to handle the partial label errors in multi-label classification. Indeed, label smoothing is a form of loss-correction [Lukasik et al., 2020] and we also prove the proposed label weighting is equivalent to directly performing the weighted average of the losses (generated from using different label sets) to form the final loss (see the proof in A.1).
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A Appendix

Due to the limited space in the main text, we want to discuss some important related issues here and meanwhile demonstrated additional experiments of the proposed attention-on-label module. It starts with a discussion about what the attention-on-label really does and follows by extensive experimental results on both CIFAR-10 and chest X-rays image datasets.

A.1 Attention-on-label Is A Form of Lost-Correction

Here, we try to demonstrate how the proposed attention-on-label module really works and discuss its connection to other prior arts. First, we present a theorem, indicating that attention weights applied on the labels can also be employed to re-weight the losses that are computed using label sets from different annotators.

**Theorem 1** (Label-Sampling Formulation). The loss computed with the model prediction \( \hat{y} \) and the sampled label \( \tilde{y} = \sum_{m=1}^{M} w_m y_m \),

\[
L_C(\hat{y}, \tilde{y}) = L_C(\hat{y}, \sum_{m=1}^{M} w_m y_m)
\]  

(6)

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is equivalent to a weighted summation of losses computed with each set of label $y_m$.

$$
L_C(\hat{y}, \tilde{y}) = \sum_{m=1}^{M} w_m L_C(\hat{y}, y_m) \tag{7}
$$

where

$$
L_C(\hat{y}, y) = -\frac{1}{N} \sum_{i=1}^{N} y_i \log \hat{y}_i + (1 - y_i) \log(1 - \hat{y}_i) \tag{8}
$$

is the binary cross-entropy loss. $w_m$ is the attention weights as defined in the main text. $N$ represents the number of classes in the label, and $M$ is the total number of label sets (annotators).

Thus, the proposed attention-on-label mechanism can be transformed to a loss re-weighting module, where the weights are the same ones that are generated from the back-propagation feedback using different label sets in the meta-training process. Indeed, it shares a similar insight with [Ren et al. (2018)] while [Ren et al. (2018)] re-weighted the losses based on the variation of input images. Similar to Theorem 1, we can also learn that re-weighting the losses is equivalent to the weighted sample of network predictions (maybe with different data samples as input). Accordingly, the noise in data (on both images and labels) can be observed and corrected via studying the losses. It also leads to a broader research topic of modeling the distribution of losses, e.g., recent work on learning with noisy label [Li et al. (2020)] by modeling the losses with Gaussian mixture models. We believe our work probably could be explored further in that direction.

Proof of Theorem 1: Recall that $\tilde{y} = \sum_{m=1}^{M} w_m y_m$ is the attention-weighted sampling of different label sets. $y_m = [y_1^m, ..., y_n^m, ..., y_M^m], y^m_n \in \{0, 1\}$ is one of the $M$ set labels.

$$
L_C(\hat{y}, \tilde{y}) = -\frac{1}{N} \sum_{i=1}^{N} [\hat{y}_i \log(\hat{y}_i) + (1 - \hat{y}_i) \log(1 - \hat{y}_i)]
$$

$$
= -\frac{1}{N} \sum_{i=1}^{N} \sum_{m=1}^{M} w_m y^m_i \log(\hat{y}_i) + (1 - \sum_{m=1}^{M} w_m y^m_i) \log(1 - \hat{y}_i)]
$$

$$
= -\frac{1}{N} \sum_{i=1}^{N} \sum_{m=1}^{M} w_m [y^m_i \log(\hat{y}_i) - y^m_i \log(1 - \hat{y}_i)] + \log(1 - \hat{y}_i)]
$$

$$
= -\frac{1}{N} \sum_{i=1}^{N} \sum_{m=1}^{M} w_m [y^m_i \log(\hat{y}_i) + (1 - y^m_i) \log(1 - \hat{y}_i) - \log(1 - \hat{y}_i)] + \log(1 - \hat{y}_i)]
$$

$$
= -\frac{1}{N} \sum_{i=1}^{N} \sum_{m=1}^{M} w_m [y^m_i \log(\hat{y}_i) + (1 - y^m_i) \log(1 - \hat{y}_i)]
$$

Since $w_m$ is computed using the softmax function and $\sum_{m=1}^{M} w_m = 1$,

$$
L_C(\hat{y}, \tilde{y}) = -\frac{1}{N} \sum_{i=1}^{N} \sum_{m=1}^{M} w_m [y^m_i \log(\hat{y}_i) + (1 - y^m_i) \log(1 - \hat{y}_i)]
$$

$$
= \sum_{m=1}^{M} w_m \left\{-\frac{1}{N} \sum_{i=1}^{N} [y^m_i \log(\hat{y}_i) + (1 - y^m_i) \log(1 - \hat{y}_i)]\right\}
$$

$$
= \sum_{m=1}^{M} w_m L_C(\hat{y}, y_m).
$$

$\square$
A.2 ADDITIONAL EXPERIMENTS ON CIFAR-10

A.2.1 DETAILS OF ADDING NOISE TO CIFAR-10 TRAINING DATA

We simulate 5 different types of annotators (with different experience) in a similar manner as Tanno et al. (2019) by injecting noise into the ground-truth label of the training set in CIFAR-10.

**Hammer-Spammer (HS):** For each class, the annotation is correct with probability $p \in [0, 1]$ and otherwise chooses labels uniformly as defined in Khetan et al. (2017).

**Structured-Flips (SF):** Similar to the HS annotator, SF is correct with a probability $p$ and otherwise we flip the label of each class to another label (as easily confused ones), which is chosen as pre-defined pairs for each class. The pairs are defined as Airplane vs Bird, cat vs dog, dear vs cat, horse vs deer, ship vs airplane, and truck vs automobile.

**Ordered-Confusion (OC):** This annotator is likely to confuse the target class with “neighbouring” classes as defined in the corresponding confusion matrix.

**Adversarial (AD):** AD is an adversarial annotator, who has an high accuracy of grouping images from the same category while constantly giving the wrong labels.

**Average (AVG):** The AVG annotation is composed using an average of all 4 confusion matrices from previously defined 4 types of annotators.

The overall noise-level is defined as $1 - p$. Each set of noisy labels are generated based on the defined confusion matrices for each type (as samples shown in Fig.4 where the noise-levels for HS, SF, OC, AD are 30%, 40%, 50%, 100% individually). Whether each data entry would have a noisy label is randomly selected while the overall noisy distribution should correspond to each confusion matrix, individually.

A.2.2 HOW DOES DIFFERENT NOISE LEVEL OF LABELS AFFECT THE PERFORMANCE?

For this experiment, we want to see how the noise-level will affect the model training and the performance of our proposed method and CM. We include 4 sets of labels, i.e., HS, SF, OC and AVG. For each time, all 4 sets share the same noise-levels (ranged from 10% to 80%). We excuse the AD label set from this experiment since its noise level can not be adjusted. We compare the prediction accuracy (in multi-class classification tasks) of baseline models (R50) that are trained using individual label sets and our proposed method. The performance of CM is also evaluated. Both CM and ours are using all 4 label sets for the training. The results are shown in Figure 5. The proposed method can constantly achieve better or similar results as the models trained with the relatively more accurate labels (e.g., AVG and HS). Furthermore, our method outperforms CM in most of the noise-levels and has even bigger margins for noise-level 40% and 50%. Additionally, we can also see that SF noise harms the performance the most since similar objects with erroneous labels can confuse the model more.

A.2.3 HOW DOES DIFFERENT NUMBER OF AVAILABLE ANNOTATION SETS AFFECT THE PERFORMANCE?

In this experiment, we try to vary the number of available label sets (from 2, 3, 4 and 5 different types of annotators) used for training the proposed model (ours) and CM at different noise level (at 10%,

Figure 4: Confusion matrices of noisy labels from 5 different types of simulated annotators.
Figure 5: Classification accuracy using different label sets and methods over a range of noise-levels.

Figure 6: Classification accuracy using different number of label sets at noise-level 10%, 30%, and 50%. We start with training model using 2 quite different label sets, i.e., HS and AD. Then we add OC, SF, and AVG one at a time to see how the increasing number of the label sets could affect the final classification performance. HS represents a relatively experienced annotators and AD can be seen as a totally ‘bad’ annotator. We start with these two sets of labels. Then, label sets from other types of annotators are added. As shown in the Figure 6, a surge of the accuracy can be observed after including more than 2 annotators. Considering that the adversarial annotator (with noise-level 100%) is among the initial two, both CM and ours can learn better immediately after a third one (as a confirmation) jumps in. We can also observe that our method performs much better when the noise level is relatively high (50% in this case), while the CNN model itself may have already been capable of learning well from the labels with low noise levels.

A.3 Baseline Classification Results with Different Annotations

As shown in Table 1, we observe a large difference in uncertainty among various algorithm generated label sets. Therefore, we first want to see how these different label sets will affect the model training. In Table 5, we illustrate the averaged AUCs for four different label sets. negbio_u0 is generated by setting all the uncertain cases to 0 (as negative cases) while negbio_u1 is produced by giving all the uncertain cases to 1 (as positive cases). Similar process is applied to the chexpert label sets as well. As shown in Table 5, the testing performance of all four models are relatively on the same level for both MIMIC-CXR and OpenI. It indicates that the CNN based model is not so sensitive to the change of labels and can overcome the noise in the label set to a certain degree, but we should note that it does not necessarily improve the overall performance of the trained model. We believe a large amount of data with higher quality labels will benefit the training and make the trained model more accurate and robust.
Table 5: Averaged AUCs with the baseline R50 from four label sets.

| Disease | AVG AUC (MIMIC-CXR) | AVG AUC (OpenI) | negbio_u1 | negbio_u0 | chexpert_u1 | chexpert_u0 |
|---------|---------------------|-----------------|-----------|-----------|-------------|-------------|
| No-finding | 0.825 | 0.821 | 0.824 | 0.810 |
| opacity | 0.751 | 0.756 | 0.755 | 0.752 |

Table 6: Classification AUCs for 14 findings in both Chest X-ray images and associated text reports using the testing set of MIMIC-CXR (with NLP generated labels) and OpenI dataset (hand-labeled GT). E-cardio: enlarged-cardiomediastinum; Pneum-x: pneumothorax

| Disease | MIMIC-CXR Test (NLP) | OpenI (hand-labeled) | Image only | Image & Text | Average |
|---------|----------------------|----------------------|------------|-------------|---------|
| Atelectasis | 0.821 | 0.832 | 0.826 | 0.833 | 0.874 | 0.781 | 0.81 | 0.826 |
| Cardi. | 0.825 | 0.852 | 0.879 | 0.913 | 0.847 | 0.859 | 0.881 | 0.879 |
| Consol. | 0.762 | 0.751 | 0.906 | - | - | 0.829 | 0.842 | 0.906 |
| Edema | 0.887 | 0.903 | 0.885 | 0.931 | 0.879 | 0.895 | 0.924 | 0.885 |
| E-cardio | 0.74 | 0.757 | 0.725 | - | - | 0.795 | 0.758 | 0.725 |
| Fracture | 0.722 | 0.771 | 0.632 | 0.671 | - | 0.513 | 0.596 | 0.632 |
| Lesion | 0.765 | 0.744 | 0.643 | 0.643 | 0.658 | 0.585 | 0.58 | 0.643 |
| Opacity | 0.814 | 0.82 | 0.775 | 0.803 | - | 0.742 | 0.738 | 0.775 |
| No-finding | 0.857 | 0.863 | 0.775 | - | 0.747 | 0.754 | 0.739 | 0.775 |
| Effusion | 0.906 | 0.914 | 0.942 | 0.942 | 0.899 | 0.912 | 0.932 | 0.942 |
| Pleural-o. | 0.866 | 0.829 | 0.705 | - | - | 0.648 | 0.676 | 0.705 |
| Pneumonia | 0.809 | 0.809 | 0.871 | 0.863 | 0.731 | 0.793 | 0.882 | 0.833 |
| Pneum-x | 0.866 | 0.858 | 0.833 | 0.843 | 0.709 | 0.793 | 0.882 | 0.833 |
| Devices | 0.92 | 0.926 | 0.729 | 0.805 | - | 0.628 | 0.655 | 0.729 |
| Average | 0.825 | 0.830 | 0.794 | - | - | 0.751 | 0.724 | 0.794 |

Table A.4: Averaged AUCs with the baseline R50 from four label sets.

A.4 ADDITIONAL EXPERIMENTS ON CHEST X-RAY IMAGES AND TEXTUAL REPORTS

In addition to the classification results using image only shown in the main text, we show the complete results for classifying the image and text together on the testing set of MIMIC-CXR (with NLP mined image labels) and OpenI (with hand-labeled labels). We observe similar results on the image-text classification task in comparison to image-only ones. The data from OpenI dataset are from a different institute to the one of MIMIC-CXR data (our training data). Therefore, the domain gap shall be considered when we examine the performance. Table 5 additionally shows the AUCs for each disease findings. Indeed, the text report contains more information about the disease diagnosis (maybe more than the image itself). We also observe increase of the overall AUCs. In this case, our proposed meta-training with attention-on-label scheme also helps to boost the classification performance with a significant amount. As pointed out before, TieNet achieves better classification results in some of the categories since they adopted a more complicated text embedding network (hard to implement with no open code released) and we believe better results could be obtained if our learning process was applied on the same model.
Table 7: Classification AUCs for 14 findings in Chest X-Ray image and text report using the testing set of MIMIC-CXR (with NLP generated labels) and MIMIC-CXR 1K hand-labeled Test data. negbio_u1, negbio_u0, chexpert_u1, and chexpert_u0 are four sets of image labels from the original NLP mined labels with uncertainty. negbio_u1 is produced by setting uncertainty -1 to 1 and we set -1 to 0 for negbio_u0. Similar settings for chexpert_u1 and chexpert_u0.

A.5 Classification Results on MIMIC-CXR 1K Hand-labeled Test Data

Following the same labeling protocol proposed in [Demner-Fushman et al., 2012], we randomly selected 1000 images and associated textual reports from the testing set of MIMIC-CXR dataset. One of our staffs (trained by a board-certified radiologist) hand-labeled the image by assigning the 14 labels manually to each image based on the associated reports. Identifying disease mentions in a report is a more accessible process comparing to examine the chest x-ray images to recognize the disease pattern in images, which will require years of professional training. The 14 labels adopted are identical to the NLP mined labels, i.e., Atelectasis, Cardiomegaly, Consolidation, Edema, Enlarged-cardiomediastinum, Fracture, Lung-lesion, Lung-opacity, No-finding, Pleural-effusion, Pleural-other, Pneumonia, Pneumothorax, and Support-devices.

As shown in Table 7 we observe the similar superior performance from our proposed method on the MIMIC-CXR 1K hand-labeled Test data. Note that the absolute accuracy is higher than the ones reported on OpenI dataset. It may indicate the domain gap between MIMIC-CXR and OpenI dataset.

Additionally, we evaluate the accuracy of NLP mined label sets, e.g., negbio_u1 and negbio_u0. negbio_u1 and negbio_u0 are two sets of image labels derived from the original NLP mined labels with uncertainty (labeled as -1). negbio_u1 is produced by setting uncertainty to 1 and we set -1 to 0 for negbio_u0. Two sets of NLP labels have quite different accuracy (6% gap) on the hand-labeled set. Similar findings can be observed between chexpert_u1 and chexpert_u0. It may be because the manual image labeling leans to the positive for those uncertain cases when our annotators will give 1 to those cases that the radiologist reported the observation of symptoms on the image (e.g., a density) while he/she is not sure what disease it is (e.g., it could be pneumonia, effusion, or consolidation). This aligns with the protocol used in [Demner-Fushman et al., 2012]. Our proposed method actually achieve a higher or similar accuracy as the NLP annotators while a model trained with NLP mined labels usually can not reach the same level of accuracy.
A.6 PSEUDO-CODE OF THE MAIN TRAINING FUNCTION

```python
def train(cls_model, bert_model, attn-on-label, args):
    for batch_idx, (images, labels_negbio_u1, labels_negbio_u0,
                 labels_chexpert_u1, labels_chexpert_u0,
                 reports) in enumerate(tqdm(train_loader)):
        cls_model.train()
        bert_model.eval()
        attn-on-label.train()
        optimizer.zero_grad()

        # computing model prediction
        text_embedding = bert_model(reports)
        preds = cls_model(images, text_feat)

        label_list = [labels_negbio_u1, labels_negbio_u0,
                      labels_chexpert_u1, labels_chexpert_u0]
        feat_all = []

        # meta-training for each set of label
        for targets_m in label_list:
            meta_loss = binary_cross_entropy_loss(preds, targets_m)

            # Meta-training for classification model
            grads = get_grad(meta_loss, cls_model.parameters())
            cls_weights = cls_model.parameters() - args.meta_lr * grads

            # Computing Image Features using Meta-trained model
            feat_tmp = cls_model(inputs, text_feat, weights=cls_weights,
                                 get_feat=True)
            feat_all.append(feat_tmp.detach())

        # attention-on-label module
        feat_all = stack(feat_all)
        attn_loss = softmax(attn-on-label.attn_fc(feat_all))
        # compute new label
        new_labels = mean(attn_loss * stack(label_list))
        # differentiable binarization
        new_labels = 1.0 / (1.0 + exp((new_labels - 0.1) * -50.0))

        class_loss = binary_cross_entropy_loss(preds, new_labels)

        # updating the attn-on-label parameters
        grads = get_grad(class_loss, attn-on-label.parameters())
        attn_weights = attn-on-label.parameters() - args.attn_lr * grad
        attn-on-label.attn_fc.weight.copy(attn_weights['attn_fc.weight'])
        attn-on-label.attn_fc.bias.copy(attn_weights['attn_fc.bias'])

        # update the classification model
        class_loss.backward()
        optimizer.step()
```

Listing 1: Train Function