Controlled Release of TGF-β3 for Effective Local Endogenous Repair in IDD Using Rat Model

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Introduction: Intervertebral disc (IVD) degeneration (IDD) is one of the most widespread musculoskeletal diseases worldwide and remains an intractable clinical challenge. Currently, regenerative strategies based on biomaterials and biological factors to facilitate IVD repair have been widely explored. However, the harsh microenvironment, such as increased ROS and acidity, of the degenerative region impedes the efficiency of IVD repair. Here, an intelligent biodegradable nanoplatform using hollow manganese dioxide (H-MnO2) was developed to modulate the degenerative microenvironment and release transforming growth factor beta-3 (TGF-β3), which may achieve good long-term therapeutic effects on needle puncture-induced IDD.

Methods: Surface morphology and elemental analysis of the MnO2 nanoparticles (NPs) were performed by transmission electron microscopy and an energy-dispersive X-ray spectroscopy detector system, respectively. The biological effects of MnO2 loaded with TGF-β3 (TGF-β3/MnO2) on nucleus pulposus cells (NPCs) were assessed via cytoskeleton staining, EdU staining, qPCR and immunofluorescence. The efficacy of TGF-β3/MnO2 on needle puncture-induced IDD was further examined using MRI and histopathological and immunohistochemical staining.

Results: The MnO2 NPs had a spherical morphology and hollow structure that dissociated in the setting of a low pH and H2O2 to release loaded TGF-β3 molecules. In the oxidative stress environment, TGF-β3/MnO2 was superior to TGF-β3 and MnO2 NPs in the suppression of H2O2-induced matrix degradation, ROS, and apoptosis in NPCs. When injected into the IVDs of a rat IDD model, TGF-β3/MnO2 was able to prevent the degeneration and promote self-regeneration.

Conclusion: Use of an MnO2 nanoplatform for biological factors release to regulate the IDD microenvironment and promote endogenous repair may be an effective approach for treating IDD.

Keywords: intervertebral disc degeneration, hollow manganese dioxide, transforming growth factor beta-3, oxidative stress, endogenous repair

Introduction

Low back pain, a leading cause of disability worldwide, is strongly associated with intervertebral disc degeneration (IDD), with IDD appearing in 40% of all cases of lower back pain.1-3 The loss of disc cell viability and functionality is thought to be critical to disrupting disc homeostasis.4 Excessive apoptosis and cellular senescence from IDD contribute to a reduced number of viable disc cells.5,6 Deficiencies in anabolic factors such as transforming growth factor beta (TGF-β) and insulin-like growth factor-1 may further reduce cellular viability and the production of extracellular matrix (ECM).7 In addition, the increased production of reactive oxygen species (ROS) and catabolic cytokines along with the accumulation of senescent disc cells may further deteriorate the microenvironment of degenerated intervertebral discs (IVDs).8 Based on these observations, the ideal biological therapeutics for IVD regeneration should provide the disc with viable and functional cells and improve the survival conditions within degenerating IVDs.9
TGF-β3, an important member of the TGF-β superfamily, is involved in the regulation of biological processes such as proliferation, survival, and differentiation.\textsuperscript{10,11} TGF-β3 upregulates the expression of genes involved in cartilage formation to promote cartilage repair and accelerate chondrogenic differentiation.\textsuperscript{12} TGF-β3 was shown to stimulate adipose-derived stem cell proliferation and chondrogenic differentiation in vitro.\textsuperscript{13} Importantly, TGF-β3 stimulation enhances cell survival and matrix deposition in the IVDs.\textsuperscript{14,15} Hence, targeting the supply of TGF-β3 could improve the metabolic imbalance of the ECM in IDD, and potentially slow its progression. However, supplying pure TGF-β3 to diseased tissues will cause local overdose, and the protein will be quickly washed away or degraded by body fluids.\textsuperscript{10} A way to deliver a sustained dose of TGF-β3 into target tissues could facilitate the IVD repair process.

Nanoparticles (NPs) have been developed as carriers for the delivery of a wide range of active pharmaceutical ingredients to overcome the limitations of free therapeutics and navigate biological barriers.\textsuperscript{16} Encapsulation in NPs can improve the stability and solubility of the cargo, promote transmembrane transport, and prolong drug circulation time, thereby increasing its safety and effectiveness.\textsuperscript{17} In recent years, manganese dioxide (MnO\textsubscript{2})-based NPs have attracted interest in the field of medical science due to their high sensitivity to H\textsubscript{2}O\textsubscript{2} and H\textsuperscript{+}, which are abundant in the tumor, osteoarthritis, and IDD microenvironments.\textsuperscript{18–20} Yang et al developed a hollow MnO\textsubscript{2} nanoplatform for the sustained release of anti-tumor drugs in a slightly acidic environment and in the presence of H\textsubscript{2}O\textsubscript{2}.\textsuperscript{21} Kumar et al reported that MnO\textsubscript{2} NPs protect cartilage from inflammation induced by oxidative stress.\textsuperscript{22} However, little is known about the involvement of MnO\textsubscript{2} NPs in the regulation of the IDD microenvironment. During IDD pathogenesis, the acidity and ROS levels within the degenerated IVDs significantly increase, which can inhibit normal cellular activity and accelerate IVD degeneration.\textsuperscript{9,23,24} Therefore, the application of MnO\textsubscript{2} NPs might improve the harsh survival conditions in the disc microenvironment as a way to promote tissue regeneration.

In this study, we prepared an intelligent drug delivery system based on hollow MnO\textsubscript{2} NPs encapsulating TGF-β3. The NPs exhibited satisfactory drug loading efficiency along with pH-responsive degradation. The hollow MnO\textsubscript{2} NPs degraded to release the encapsulated TGF-β3 when exposed to excessive H\textsubscript{2}O\textsubscript{2} and/or H\textsuperscript{+} in tissues and cells. The released TGF-β3 improved cell survival and ECM deposition by scavenging ROS, thereby alleviating the progression of
IDD. Based on these results, the hollow MnO$_2$-based responsive nanocarriers for drug delivery show promise for IVD repair.

**Materials and Methods**

**Synthesis and Characterization of Hollow MnO$_2$ Nanoparticles**

Hollow MnO$_2$ NPs were prepared as previously described.$^{21,25}$ Briefly, solid SiO$_2$ (sSiO$_2$) NPs were first synthesized as follows: 14 mL of ethanol, 2 mL of deionized water, and 500 μL of NH$_3$·H$_2$O were mixed in a 50-mL round-bottom flask. The mixture was heated under magnetic stirring in an oil bath at 50 °C for 5 min. 500 μL of tetraethyl orthosilicate was then added dropwise and the mixture was stirred at 50 °C for 2 h to produce sSiO$_2$ NPs. The resulting sSiO$_2$ NPs were washed twice with ethanol and twice with water and then stored in water for further use. For the synthesis of sSiO$_2@$MnO$_2$ NPs, 600 mg of KMnO$_4$ dispersed in 20 mL of water was added dropwise into the sSiO$_2$ NPs during sonication. The mixture was ultrasonicated for 1 h, then stirred overnight at room temperature. The resulting sSiO$_2@$MnO$_2$ NPs were washed three times with deionized water and centrifuged at 14,800 rpm/min. Finally, the prepared sSiO$_2$ coated with mesoporous MnO$_2$ was dissolved in Na$_2$CO$_3$ at 60 °C for 12 h. The resulting hollow MnO$_2$ NPs were then centrifuged and washed several times with water. The surface morphology and elemental analysis of the NPs were determined by transmission electron microscopy (TEM; FEI Tecnai F20, Hillsboro, OR, USA) and an energy-dispersive X-ray spectroscopy detector system (EDS, Oxford X-MAX, Oxford, UK), respectively.

**Encapsulation of TGF-β3 into Hollow MnO$_2$ Nanoparticles**

For TGF-β3 loading, hollow MnO$_2$ NPs (5 mg) were added into 1 mL of phosphate-buffered saline (PBS; pH 7.4) containing TGF-β3 (1 μg; Sigma-Aldrich, St. Louis, MO, USA) and stirred for 12 h at room temperature. Subsequently, the NPs were centrifuged, and the supernatant was removed.

**Examination of in-vitro Release of TGF-β3 from MnO$_2$ Nanoparticles**

The release of TGF-β3 from the NPs in vitro was quantified by ELISA (Sangon Biotech, Shanghai, China). The NPs were incubated in 1 mL of PBS at different pH values (6.5 and 7.4) in the absence or presence of 100 μM H$_2$O$_2$. At predetermined time points, the samples were centrifuged, the supernatant was collected, and an equal amount of fresh PBS was added to continue the release process. All collected solutions were kept frozen at −20°C for subsequent analysis with TGF-β3-ELISA.

**Isolation and Culture of Nucleus Pulposus Cells**

To isolate nucleus pulposus cells (NPCs), six-week-old male Sprague-Dawley rats were sacrificed and their lumbar and caudal IVDs were harvested under aseptic conditions. We then separated gel-like nucleus pulposus tissues from the discs and treated them with 0.25% (w/v) type II collagenase (Yeasen, Shanghai, China) for 4 h at 37 °C. The obtained cell suspension was centrifuged at 1200 rpm for 3 min and then cultured with DMEM/F12 containing 10% fetal bovine serum (HyClone, Logan, UT, USA) and 1% penicillin/streptomycin (Gibco, Grand Island, NY, USA) in a humidified incubator at 37 °C with 5% CO$_2$. NPCs at passage 2 were used for all of the experiments in this study.

**Cell Culture**

NPCs at passage 2 were plated on a cell culture dish at an initial density of 5000 cells/cm$^2$. When the cells were attached, H$_2$O$_2$ solution was diluted with DMEM/F12 medium and then added into the dishes to a final concentration of 100 μM to induce oxidative stress in the NPCs. To further investigate whether NPs altered oxidative stress, after treatment with H$_2$O$_2$ for 12 h, the medium was replenished by fresh medium containing TGF-β3, MnO$_2$, and TGF-β3/MnO$_2$ for 24 h, respectively.

**In vitro Cytotoxicity Assay**

The cell toxicity of the NPs was determined by examining the viability of NPCs treated with NPs using a CCK-8 assay (NCM Biotech, Suzhou, China). Briefly, cells (5×10$^3$ per well) were seeded into 96-well plates and cultured for 12 h to
allow cell attachment. The cells were then incubated with a series of increasing concentrations of hollow MnO$_2$ NPs for 24 h. After incubation, the cell medium was removed and replaced with 100 μL of culture medium and 10 μL of CCK-8 reagent for another 2 h for color development. Optical density was measured using a microplate reader (BioTek, VT, USA) at 450 nm.

Cellular Uptake Experiments
To assess the cellular uptake efficiency of the NPs, bovine serum albumin (BSA), and fluorescein isothiocyanate-labeled BSA (FITC-BSA; Solarbio, Beijing, China) were encapsulated into hollow MnO$_2$ NPs. After encapsulation, NPCs (5×10$^3$ per well) were cultured in 48-well plates at 37 °C for 12 h. After complete adhesion, the cells were washed twice with PBS followed by the addition of 100 μL of fresh medium containing NPs loaded with BSA or FITC-BSA. Incubation was then continued for 12 h. Next, the cells were washed three times with PBS to remove the residual NPs, fixed with 4% paraformaldehyde solution for 15 min, and stained with TRITC-phalloidin and DAPI. Finally, images were obtained using a fluorescence microscope.

Intracellular ROS Assay
An ROS assay kit (Beyotime, Shanghai, China) was used to measure the accumulation of intracellular ROS in the treated cells. The cells were first exposed to DCFH-DA solution (10 μM) and then incubated for 1 h at 37 °C. After a wash with PBS, the fluorescence of the cells was observed using a fluorescence microscope.

Cell Proliferation Assay
Cell proliferation was measured using a BeyoClick™ EdU Cell Proliferation Kit with Alexa Fluor 488 (Beyotime, Shanghai, China). Briefly, immediately before H$_2$O$_2$ treatment in all groups, EdU was added to label cells undergoing active DNA synthesis. After 6 h, the cells were fixed in 4% paraformaldehyde for 15 min and permeabilized with 0.3% Triton X-100 in PBS for 10 min. Subsequently, the samples were incubated with click reaction solution at room temperature for 30 min, and the nuclei were counterstained with Hoechst 33342 dye. Images were acquired using a fluorescence microscope.

Quantitative Polymerase Chain Reaction Analysis
TRIzol reagent (Invitrogen, Carlsbad, CA, USA) was used to extract the total RNA from NPCs under different conditions. The RNA concentrations were measured using a NanoDrop 2000 spectrophotometer (Thermo Fisher Scientific, Waltham, MA, USA). RNA (1 μg) was reverse-transcribed into cDNA using a 5X All-In-One RT MasterMix (abm, Vancouver, BC, Canada) according to the manufacturer's instructions. Subsequently, qPCR was performed using iQ SYBR Green Supermix (Bio-Rad, Hercules, CA, USA). The primer sequences (Sangon Biotech, Shanghai, China) of the genes used in this study are listed in Table 1. The expression of each gene was normalized by the housekeeping gene GAPDH. Relative changes in mRNA level were analyzed using the $2^{-\Delta\Delta CT}$ method.

Immunofluorescence
NPCs were fixed in 4% paraformaldehyde for 15 min and then permeabilized with 0.3% Triton X-100 in PBS for 10 min. Non-specific binding was blocked by a commercial blocking reagent (Beyotime, Shanghai, China) followed by primary antibodies incubation at 4 °C overnight (rabbit anti-Col-II, rabbit anti-iNOS, Abcam, Cambridge, UK). After overnight incubation, samples were incubated with second antibodies (Beyotime, Shanghai, China) for 1 h. Nuclei were stained with DAPI and images were acquired using a fluorescence microscope. Semi-quantitative fluorescence analysis was performed using Image J software (NIH, Bethesda, MD, USA).

Examination of Caudal Full (Form of IDD) Using Rat Model
All procedures followed the NIH Guide for the Care and Use of Laboratory Animals and were approved by the Institutional Animal Care and Use Committee of Soochow University. After complete anesthesia, the rat tails were disinfected, and Co7-8 IVDs were punctured sequentially with 21G needles to induce degeneration. To ensure that
trauma was induced, a needle was used to puncture the center of the discs, rotated for 5 s then the position maintained for 30 s. Each disc was then injected with 20 µL of material by a 33 G needle; in the negative control group, the discs were injected with PBS instead of NPs. After surgery, the rats were placed in a warm and ventilated location.

**Magnetic Resonance Imaging**

Four and eight weeks after surgery, the water contents of the IVDs were evaluated on magnetic resonance imaging (MRI, 3.0 T; Siemens, Germany) based on the signal intensity in sagittal T2-weighted images. The MRI images were evaluated by another blinded researcher using the classification for intervertebral disc degeneration (Table 2), as previously reported.26

**Histopathological and Immunohistochemical Analysis of Intervertebral Disc Regeneration**

After sacrifice, the IVDs were removed from each rat and placed in 10% formalin for 48 h, decalcified in 10% EDTA for 30 d, and then embedded in paraffin blocks. The specimens were cut into 5-µm-thick histopathological sections followed by staining with either H&E or Safranin-O/Fast Green. The histopathological grade was calculated as described in previous work27 and the specific definition of histopathological grade was shown in Table 3. To observe the expressions of type II collagen and iNOS in the harvested tissues, the sections were immunohistochemically stained for collagen type II and iNOS (Abcam, Cambridge, UK). Semi-quantitative immunohistochemical stain analysis was performed using Image J software.

| Table 1 Primers for qPCR |
|--------------------------|
| Gene | Forward (5'-3') | Reverse (5'-3') |
| SOD1 | CGGCTTCTGCTGTCCTCCCTGC | AACTGGTCGCCCGCTGGCTTC |
| SOD2 | GCTGGAGGGCTATCAAGCGTGAC | TTAGAGGCAGGCGGAATCTGTAAG |
| CAT | GCCCTGACTGACGGGCAGTTGC | CTGGCTCTCCACTGTCTCATCTG |
| Adamts5 | TCTCTGGTGCTGACTCTTCCC | TGGTTCTGCTGCTGATGAGCTG |
| MMP3 | CAGTCTGCTGCTGGCTGTGAC | AACTCCATGCCAGCAGCTCTCC |
| BAX | CACAGCTCTGAAACAGATCATGA | TCACGCCATCTTCTCCAGATGTT |
| Col-II | AGCCTCAAGTGCCTGAAACACACC | ATCCAGTACTCCGGCTCTCCAC |
| iNOS | GAGACGCACAGGCAGAGGTTG | CAGGAGAGCAGCCACAC |
| COX-2 | TCTCGATGCTGCTGCTTGCATGACTG | CCCTGTCAAGAGGAGGTGAGGAGT |
| ACAN | GCGCTCCTGCTGCTGCTGCTGCTG | GGCGTCCAAAACAAACCGAGAG |
| MCL1 | TCACTCTCCGGCTACCTGC | ACTCACAACCAGCAGCTCC |
| BCL2 | CACCATCCGGACATCTTCTCTTT | AGCGTCTTCAGAGACAGCCAG |
| GAPDH | GACATGCCGGCTGGAGAAAC | AGCCAGGATGCCCCCTTGA |

| Table 2 Classification of Disc Degeneration |
|-------------------------------------------|
| Grade | Structure | Distinction of Nucleus and Annulus | Signal Intensity | Height of Intervertebral Disc |
|-------|-----------|-----------------------------------|----------------|-----------------------------|
| I     | Homogeneous, bright white | Clear | Hyperintense, iso intense to cerebrospinal fluid | Normal |
| II    | Inhomogeneous with or without horizontal bands | Clear | Hyperintense, iso intense to cerebrospinal fluid | Normal |
| III   | Inhomogeneous, gray | Unclear | Intermediate to hypointense | Normal to slightly decreased |
| IV    | Inhomogeneous, gray to black | Lost | Intermediate to hypointense | Normal to moderately decreased |
| V     | Inhomogeneous, black | Lost | Hypointense | Collapsed disc space |
Statistical Analysis
All data are expressed as mean ± standard deviation. Statistical significance was evaluated using a one-way analysis of variance (GraphPad Software, USA) with Tukey’s multiple comparison test to further evaluate differences between groups. *P* values less than 0.05 were considered statistically significant.

Results

Synthesis and Characterization of MnO$_2$ Nanoparticles
The MnO$_2$ NPs were successfully synthesized and used as carriers for TGF-β3 delivery. The TEM images of the MnO$_2$ NPs clearly show the spherical morphology and hollow structure of the product, and the thickness of the MnO$_2$ shell was approximately 15 nm (Figure 1A). The corresponding EDS spectrum proved the presence of the Mn and O elements derived from MnO$_2$ and also confirmed the hollow structure of MnO$_2$ without element Si (Figure 1B). In addition, the cytotoxicity of the MnO$_2$ NPs was tested by CCK-8 assay, which found that the MnO$_2$ NPs did not exhibit obvious toxicity to NPCs, even at high concentrations up to 50 μg/mL (Figure 1C). Hence, the MnO$_2$ NPs were used at a concentration of 50 μg/mL in further experiments.

The Critical Examination of Controlled Drug Release
MnO$_2$ is known to be stable under neutral and basic conditions; however, it decomposes into Mn$^{2+}$ under low pH. A release test was performed to evaluate the degradation and loading of MnO$_2$ at different pH values (7.4 and 6.5) in the absence or presence of 100 μM H$_2$O$_2$ for various treatment times lengths (Figure 2). The release curve shows that TGF-β3 was continuously released from MnO$_2$ in a time-dependent manner. Compared with the slow drug release observed at pH 7.4, the rate of TGF-β3 release was higher at pH 6.5. Furthermore, incubation with H$_2$O$_2$ at pH 6.5 further accelerated drug release by triggering the decomposition of the MnO$_2$ nanocarriers into Mn$^{2+}$ ions.

In vitro Cellular Uptake of MnO$_2$ Nanoparticles
The endocytosis of NPs in NPCs was investigated by loading FITC-BSA into the MnO$_2$ NPs. As shown in Figure 3, the fluorescence signal of the FITC-BSA-loaded MnO$_2$ NPs was strong, indicating that the MnO$_2$ NPs had excellent drug-loading ability. In particular, the fluorescence signal was primarily located in the cytoplasm with some signal found in the nucleus. This confirmed the high cellular uptake of MnO$_2$ NPs.

| Category | Grade |
|----------|-------|
| I. Cellularity of the annulus fibrosus | 1. Fibroblasts comprise more than 75% of the cells |
| II. Morphology of the annulus fibrosus | 1. Well-organized collagen lamellae without ruptured or serpentine fibers |
| III. Border between the annulus fibrosus and nucleus pulposus | 1. Normal, without any interruption |
| IV. Cellularity of the nucleus pulposus | 1. Normal cellularity with stellar shaped nuclear cells evenly distributed throughout the nucleus |
| V. Morphology of the nucleus pulposus | 1. Round, comprising at least half of the disc area in midsagittal sections |
Antioxidant Activity of TGF-β3-Loaded MnO₂ Nanoparticles (TGF-β3/MnO₂) Against H₂O₂

To investigate the ROS scavenging activity of TGF-β3/MnO₂, the DCF fluorescence intensity was detected using an ROS assay kit. The ROS content increased after H₂O₂ treatment, but decreased following treatment with MnO₂ and TGF-β3/MnO₂. However, treatment with TGF-β3 did not significantly reverse H₂O₂-induced ROS production (Figure 4A). In addition, the expressions of the antioxidative genes SOD1, SOD2, and CAT were significantly increased in cells treated with MnO₂ and TGF-β3/MnO₂ compared to cells treated with H₂O₂ and TGF-β3 (Figure 4B–D). Hence, the antioxidant activity of TGF-β3/MnO₂ was mainly attributed to MnO₂.

Anti-Apoptotic and Proliferative Effects of TGF-β3/MnO₂ Against H₂O₂

We evaluated the anti-apoptotic effects of TGF-β3/MnO₂ against H₂O₂ using the expression of the apoptotic gene BAX and the anti-apoptotic genes BCL2 and MCL1 in cultured NPCs. The expression of BAX was enhanced in H₂O₂-treated cells compared to the control NPCs. In contrast, the enhanced expression of the BAX gene was significantly reduced by treatment with TGF-β3, MnO₂, or TGF-β3/MnO₂, with TGF-β3/MnO₂ producing the greatest decrease in BAX expression (Figure 5A). Compared to the cells treated with H₂O₂, the expression of BCL2 and MCL1 was significantly increased by treatment with TGF-β3, MnO₂, or TGF-β3/MnO₂, with TGF-β3/MnO₂ resulting in the highest expressions (Figure 5B and C). Further, EdU assay showed that cell proliferation rate, represented by the percentage of EdU-positive cells, was decreased to 9.6% in H₂O₂-treated cells. Interestingly, this number was significantly increased to 17.6% and 18.5% in following treatment with MnO₂ and TGF-β3, respectively, and it was markedly enhanced to 28.4% in the setting of TGF-β3/MnO₂ (Figure 5D and E).

![Synthesis and characterization of MnO₂ NPs](image-url)
Characterization of the Metabolic Effects of TGF-β3/MnO₂

The above results suggest that TGF-β3/MnO₂ exerted antioxidant, anti-apoptotic, and proliferative activities to protect cells from H₂O₂ damage. To further explore the effects of TGF-β3/MnO₂ on ECM synthesis in NPCs treated with H₂O₂, we conducted qPCR measurements to investigate the expressions of genes related to anabolism, inflammation, and...
catabolism. Of the studied treatments, TGF-β3/MnO\textsubscript{2} had the best ability to reverse the H\textsubscript{2}O\textsubscript{2}-induced expression of the ECM genes Col-II and ACAN (Figure 6A and B). Further, TGF-β3/MnO\textsubscript{2} almost completely blocked the stimulatory effect of H\textsubscript{2}O\textsubscript{2} on the expressions of the pro-inflammatory enzymes COX-2 and iNOS (Figure 6C and D) and the catabolic genes MMP3 and Adamts5 (Figure 6E and F). Immunofluorescent experiments also confirmed that Col-II associated fluorescence intensity in the TGF-β3/MnO\textsubscript{2} group, was highest of the experimental groups (Figure 7A and B). Meanwhile, lower fluorescence intensity of iNOS was observed after TGF-β3/MnO\textsubscript{2} treatment (Figure 7C and D).

**In vivo Evaluation of Intervertebral Disc Regeneration by TGF-β3/MnO\textsubscript{2}**

To assess the in vivo effect of TGF-β3/MnO\textsubscript{2} treatment, a rat disc puncture model was established. PBS, MnO\textsubscript{2}, TGF-β3, or TGF-β3/MnO\textsubscript{2} was injected into the rat IVDs after they were punctured with a 21G needle. The therapeutic efficacy was evaluated based on changes in the gross appearance (Figure 8A) and MRI images (Figure 8B). After puncture, the gross appearance and T2-weighted MRI signal intensity of the IVDs were similar in the sham group and the group treated with TGF-β3/MnO\textsubscript{2}. In contrast, discs treated with PBS, MnO\textsubscript{2}, and TGF-β3 lost their signal, and water was observed (Figure 8C and D). The morphologies of the discs in each group were also evaluated with H&E (Figure 9A) and Safranin O-Fast Green staining (Figure 9B). In the sham group, the discs contained elliptical nucleus pulposus (NP), well-organized collagen lamellae, and a clear boundary between the annulus fibrosus (AF) and NP. From four to eight weeks after puncture, the size of the NP region and proteoglycan content decreased in the TGF-β3/MnO\textsubscript{2} group; however, these changes were relatively minor compared to the other experimental groups, and a clear tissue boundary between the AF and NP was still observed. In the PBS, MnO\textsubscript{2}, and TGF-β3 groups, the discs displayed degenerative characteristics such as decreased NP size and disorganized collagen fibers in the inner AF. The histopathological scores of the TGF-β3/MnO\textsubscript{2} group were significantly lower after 4 weeks, which were closest to the Ctrl group. Conversely, the histopathological scores of the other experimental groups were significantly higher, a difference that was more obvious at week 8 (Figure 9C and D).

Finally, to verify the effectiveness of TGF-β3/MnO\textsubscript{2}, the expressions of iNOS and Col-II in the IVD tissue were further evaluated using immunohistochemistry. The expression of iNOS was significantly lower in the TGF-β3/MnO\textsubscript{2}...
group than in the other experimental groups (Figure 10A). Conversely, the expression of Col-II, an important marker of ECM in the NP, was significantly higher in the TGF-β3/MnO\(_2\) group than in the other experimental groups (Figure 10B). Semi-quantitative analysis of the staining further illustrated these differences (Figure 10C and D). Therefore, from a macroscopic perspective, the in vivo experimental results indicate that the TGF-β3/MnO\(_2\) group had superior MRI signal and gross appearance compared with the other experimental groups. At the microscopic level, immunohistochemical staining revealed more residual NP, lower iNOS expression, and significantly higher Col-II expression in the TGF-β3/MnO\(_2\) group. This indicates that the imbalance in ECM synthesis in IDD, which is one of the main causes of

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**Figure 5** Anti-apoptotic and proliferative effects of TGF-β3/MnO\(_2\). qPCR analyses of the relative expression of apoptotic (BAX) (A) and anti-apoptotic (MCL1 and BCL2) (B and C) genes of NPCs in the Ctrl, H\(_2\)O\(_2\), MnO\(_2\), TGF-β3, and TGF-β3/MnO\(_2\) groups, respectively. (D) Representative images of EdU staining of NPCs in the Ctrl, H\(_2\)O\(_2\), MnO\(_2\), TGF-β3, and TGF-β3/MnO\(_2\) groups, respectively. Green represents EdU-labeled proliferating cells and blue represents nuclei. (E) Quantification of the percentage of EdU-positive cells in the Ctrl, H\(_2\)O\(_2\), MnO\(_2\), TGF-β3, and TGF-β3/MnO\(_2\) groups, respectively. *, p<0.05.
the loss of IVD function, can be reversed, thereby delaying the progression of IVD degeneration. This effect was attributed to the ability of the MnO$_2$ NPs to create an appropriate microenvironment/vehicle for TGF-β3 delivery to the IVDs. Moreover, TGF-β3 delivered via the MnO$_2$ system effectively promoted cell proliferation and inhibited ECM degradation by reducing the acidity and scavenging ROS of the IVD microenvironment.

**Discussion**

We have proposed a novel strategy for IDD treatment using a MnO$_2$ nanoplatform that effectively releases TGF-β3 in response to the acidic microenvironment produced by IDD. This novel nanoplatform can also decrease ROS accumulation to further promote cell survival and endogenous repair. The mechanisms and effectiveness of the proposed therapeutic system were validated both in vitro using rat NPCs and in vivo using a rat IDD model. Growing evidence suggests that the progression of IDD is accompanied by a pronounced decline in cell density. During aging and degeneration, excessive cellular senescence and death prevent the natural repair processes from occurring, exacerbating IDD. Anti-senescent therapy appears to have a curative effect on IDD. Regenerative medicine has emerged as a promising option for the prevention or even reversal of disc degeneration. Growth factors, which are an important component of regenerative medicine, act as mediators of the healing processes and represent potential molecular targets for stimulating and guiding regeneration. TGF-β3 plays an essential role in cell differentiation, cell adhesion, and ECM formation; TGF-β3 has been shown to promote the repair of cartilaginous

![Figure 6](image-url)
Figure 7 Immunofluorescent analysis of Col-II and iNOS expression in NPCs. Representative images of the immunofluorescence of Col-II (A) with semi-quantitative analysis (B) and iNOS (C) with semi-quantitative analysis (D) in the NPCs of the Ctrl, H$_2$O$_2$, MnO$_2$, TGF-β3, and TGF-β3/MnO$_2$ groups, respectively. Red, green and blue colors indicate Col-II protein, iNOS protein and DAPI fluorescence, respectively. *, p<0.05.
organs including IVDs and upregulate the expressions of aggrecan and type II collagen. Peck et al reported that TGF-β3 enhanced cell survival and ECM synthesis of mesenchymal stem cells in low-oxygen and nutrient-limited microenvironments. Ashraf et al reported that TGF-β3 enhanced the ability of NPCs to form tissues, in part by decreasing cell death. Consistent with the results of the present study, TGF-β3 treatment blocked the inhibitory effect of H₂O₂ on NPC proliferation, likely by suppressing the apoptotic gene BAX and upregulating the proliferative genes MCL1 and BCL2. Further, TGF-β3 alleviated the H₂O₂-induced expression of ECM genes (ACAN and Col-II) and partly blocked the stimulatory effect of H₂O₂ on the expression of catabolic (MMP3 and Adamts5) and inflammatory genes (COX-2 and iNOS). Interestingly, the protective effect of TGF-β3 against H₂O₂ damage in NPCs was independent of the inhibition of oxidative stress, as evidenced by the lack of any effect of TGF-β3 on intracellular ROS and antioxidant...
genes. In a rat model of IDD induced by needle puncture, the reductions in water and Col-II contents were attenuated by TGF-β3 treatment, which is consistent with the recovery of the MRI signal at four weeks after injection. Regrettably, the effectiveness of TGF-β3 was diminished at 8 weeks after injection, as evidenced by decreased in NP area and ECM content. This is likely because growth factors are prone to degradation in the body. Furthermore, the iNOS expression was higher in the group treated with TGF-β3 alone compared to the sham group at both time points (4 w and 8 w). This may represent an increased inflammatory response and persistent oxidative stress within the IDD microenvironment, which may be another important reason why the positive effects of TGF-β3 attenuate over time.

Increasing evidence suggests that the harsh disc microenvironment inhibits the self-healing processes of degenerating IVDs and restricts the capacity for external intervention. Oxidative stress has been identified as a major risk component of pathological mechanism behind IDD. Oxidative stress increases the concentration of ROS, which is closely related to cell senescence and apoptosis. Further, oxidative stress enhances the degradation of the ECM and the inflammatory response in IVD cells and damages the mechanical function of the IVDs. These effects accelerate the progress of IDD and lead to low back pain. Disc degeneration has long been associated with increased acidity. The pH value of normal discs is 7.2, while the pH in severely degenerated discs is 6.2. A normal pH is necessary to maintain cellular functions, while an excessively acidic environment significantly inhibits cell viability and matrix synthesis. Gilbert et al reported that the increased pH was associated with decreased NPC proliferation and vitality, a shift towards matrix catabolism, and an increased expression of proinflammatory cytokines and pain-related factors. Therefore,
targeting oxidative stress or acidity to improve the harsh microenvironment of disc degeneration may provide a new strategy for IDD treatment.

Based on the above considerations, MnO$_2$ nanostructures that are decomposed in the presence of H$^+$ or glutathione have attracted our attention. MnO$_2$ nanostructures are also able to trigger the decomposition of H$_2$O$_2$ into water and oxygen. These characteristics enhance the therapeutic potential of the nanostructure, in particular as anti-tumor and anti-osteoarthritis vectors. However, to the best of our knowledge, MnO$_2$ nanostructures have not yet been reported as a strategy for IDD therapy. In this study, we developed an intelligent nanoplatform based on MnO$_2$ NPs for TGF-$\beta$3 delivery. The nanoplatform exhibited an ultrasensitive pH-triggered release and H$_2$O$_2$-responsive oxygen generation to relieve IVD hypoxia and reduce oxidative injury, resulting in long-term therapeutic effects. We successfully synthesized spherical MnO$_2$ NPs with hollow structures. The NPs exhibited no obvious toxicity to the NPCs, even at high concentrations up to 50 $\mu$g/mL. The NPs were highly effective at drug loading. The encapsulated drug was precisely and controllably released upon exposure to H$^+$ or H$_2$O$_2$. In vitro experiments demonstrated that TGF-$\beta$3/MnO$_2$ had antioxidant and anti-apoptosis effects and promoted cell proliferation. Although TGF-$\beta$3 did not increase the antioxidant capacity of MnO$_2$, the proliferative effect of TGF-$\beta$3 was enhanced by MnO$_2$. There was increased production of ECM components (eg, ACAN and Col-II) in the presence of H$_2$O$_2$ in cells treated with TGF-$\beta$3/MnO$_2$ compared to those treated with TGF-$\beta$3 alone. We hypothesized that the enhanced effects of TGF-$\beta$3 in the setting of MnO$_2$ may be related

Figure 10 Immunohistochemical analysis of iNOS and Col-II expression in each group. Representative images of the immunohistochemical staining of iNOS (A) and Col-II (B) at 4 and 8 weeks after surgery, and the semi-quantitative analysis of iNOS (C) and COL-II (D) at these timepoints. *, p<0.05.
to the elimination of H$_2$O$_2$ by MnO$_2$, resulting in a better environment for cell survival. This effect may be derived from the reduction in inflammatory factors and catabolic makers.

To further investigate the role of TGF-β3/MnO$_2$ in vivo, an IDD model was established in rats by needle puncture with half penetration. Needle puncture is the most common method used to establish injury models because of its repeatability and short-term degenerative changes. Our in vivo results showed that needle puncture induced rapid and severe disc degeneration, as indicated by the disappearance of the nucleus pulposus area and the imbalanced ECM. These altered morphological features were almost recovered at four weeks after treatment with TGF-β3/MnO$_2$. Further, the MRI signal intensity and nucleus area were larger in the TGF-β3/MnO$_2$ group compared to the TGF-β3 and MnO$_2$ groups. Additionally, TGF-β3/MnO$_2$ effectively slowed Col-II degradation and iNOS expression for up to eight weeks after treatment, which was not observed in the TGF-β3 and MnO$_2$ groups. These findings reveal that MnO$_2$ contributes to eliminating oxidative stress and controlling the release of TGF-β3, and the latter promoted cell survival, ECM deposition and enhanced endogenous repair.

The present study has some limitations. First, we only examined the effects of TGF-β3/MnO$_2$ on the rat IDD model for eight weeks. A longer study period is needed to evaluate the long-term efficacy of the nanoplatform. Second, an upright model that is more similar to a human IDD should be used to further validate the results obtained in the rat IDD model. Third, the use of PBS solution as a vehicle increases the possibility of leakage. Thus, a better vehicle such as a hydrogel should be developed to improve drug bioavailability and avoid burst drug release.

**Conclusion**

In summary, we fabricated hollow mesoporous MnO$_2$ NPs loaded with TGF-β3 as a multifunctional drug delivery system that is responsive to H$^+$ and H$_2$O$_2$ in the IDD microenvironment. This nanoplatform can modulate the microenvironment to prolong the effects of TGF-β3, which achieved well persistent influence in IDD injury. Further studies will be needed to explore some suitable vehicles to enhance the curative effect and longer treatment periods to confirm the long-term efficacy of the nanoplatform. This injectable nanoplatform for controlled drug release provides a new strategy for tissue regeneration under local oxidative stress and acidic microenvironments.

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**Disclosure**

No potential conflict of interest was reported by the authors.

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