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Brain Network Adaptability across Task States

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Abstract

Activity in the human brain moves between diverse functional states to meet the demands of our dynamic environment, but fundamental principles guiding these transitions remain poorly understood. Here, we capitalize on recent advances in network science to analyze patterns of functional interactions between brain regions. We use dynamic network representations to probe the landscape of brain reconfigurations that accompany task performance both within and between four cognitive states: a task-free resting state, an attention-demanding state, and two memory-demanding states. Using the formalism of hypergraphs, we identify the presence of groups of functional interactions that fluctuate coherently in strength over time both within (task-specific) and across (task-general) brain states. In contrast to prior emphasis on the complexity of many dyadic (region-to-region) relationships, these results demonstrate that brain adaptability can be described by common processes that drive the dynamic integration of cognitive systems. Moreover, our results establish the hypergraph as an effective measure for understanding functional brain dynamics, which may also prove useful in examining cross-task, cross-age, and cross-cohort functional change.

Introduction

An essential characteristic of the human brain is the ability to transition between functional states in synchrony with changing demand. A central focus in neuroscience involves quantifying this adaptability and understanding the underlying brain organization that supports it. Several studies have accomplished this with functional MRI techniques by delineating changes in regional blood-oxygen-level-dependent (BOLD) signal associated with different cognitive tasks, or between task states and task-free (resting [1,2]) states [3,4]. However, this approach, which examines the magnitude of brain activity alone, is unable to completely describe the complex correlation structure linking spatially segregated neural circuits. In particular, while providing crucial insight into the spatial structure and anatomical distribution of functional activity and how it differs between task and resting states, these methods are not well suited to probe the intrinsic organization of the dynamics of task-driven transitions between cognitive states, or co-evolving associations among brain regions throughout a particular task.

Recent advances in network science provide tools to represent and characterize the functional interactions between brain regions forming cognitive systems. In this formalism, brain regions are represented as network nodes and functional connections (estimated by statistical similarities between BOLD signals [5]) are represented as network edges [6,7]. These approaches enable the statistically principled examination of large-scale neural circuits underlying cognitive processes, and have enabled quantitative comparisons between circuits [8,9]. Indeed, a growing literature provides evidence that individual tasks may elicit specific functional connectome configurations [10], while maintaining a relatively stable functional backbone reminiscent of the connectome configuration evident in the resting state [11].

Nevertheless, these studies have focused on examining task or cognitive states as separate and independent entities, and tools to quantify how brain networks reconfigure between these task states remain significantly underdeveloped. Initial efforts to examine reconfiguration properties of brain networks have focused on quantifying properties of dynamic functional connectivity at rest [12]. A relatively few studies have begun to examine reconfigu-
Author Summary

The human brain is a complex system in which the interactions of billions of neurons give rise to a fascinating range of behaviors. In response to its changing environment—for example, across situations involving rest, memory, focused attention, or learning—the brain dynamically switches between distinct patterns of activation. Despite the wealth of neuroimaging data available, the immense complexity of the brain makes the identification of fundamental principles guiding this task-based organization of neural activity a distinct challenge. We apply new techniques from dynamic network theory to describe the functional interactions between brain regions as an evolving network, allowing us to understand these time-dependent interactions in terms of organizing characteristics of the whole network. We examine patterns of neural activity during rest, an attention-demanding task, and two memory-demanding tasks. Using network science techniques, we identify groups of brain region interactions that change cohesively together over time, both across tasks and within individual tasks. By developing tools to analyze the size and spatial distributions of these groups, we quantify significant differences between brain network dynamics in different tasks. These tools provide a promising method for investigating how the changing brain network properties of individuals correspond to task performance.

In this paper, we ask a complementary set of questions that focus on sets of functional connections rather than on the entire functional connectome pattern. We ask whether sets of functional connections evolve independently within or across brain states, or whether they evolve cohesively, each set controlled by a common regulatory driver. To answer this question, we employ recently developed dynamic network science methods to estimate brain functional networks in one-minute time intervals as 86 participants engage in four task states: a task-free resting state, an attention-demanding state, and two memory-demanding states. We treat the evolving patterns of functional connectivity as temporal, or dynamic, networks [14,15,18,19,21,22] and estimate the pairwise correlation between the strengths of functional interactions over time in order to identify groups of functional interactions which display similar changes in strength within and across task states. These groups of network edges with similar dynamic patterns, known as hyperedges, have been used to quantify the co-evolution in functional brain networks over the course of a learning task [23]. Our goal is to adapt this dynamic network science method to investigate the organization of evolving functional correlations both within and between task-specific cognitive states, using hyperedges as a measure of co-evolution. We hypothesize that overall, functional interactions between brain regions especially important for particular tasks are likely to be grouped in hyperedges with interactions between regions used strongly in other tasks, capturing co-evolution between task-specific functional networks as they turn off or on together when switching tasks. Furthermore, we expect that those functional correlations that link sets of brain regions whose coordination is crucial to a particular task will be more likely to co-evolve significantly during that task alone.

In this paper, we demonstrate the existence of hyperedges driven by significant co-evolution within groups of functional interactions, both within and across task states. We develop novel network diagnostics to characterize hyperedges according to their structure, anatomy, and task-specificity. These analyses provide a unique window into the adaptability of the brain as it transitions between states and offer quantitative statistics for the comparison of such adaptability across subject cohorts.

Methods

Ethics Statement

Informed written consent was obtained from each subject prior to experimental sessions. All procedures were approved by the University of California, Santa Barbara Human Subjects Committee.

Tasks

Subjects engaged in a resting-state (task-free) period, as well as three separate tasks designed to engage different cognitive skills and task-specific brain networks: two separate functional runs of the same attention-demanding task, a memory task with lexical stimuli, and a memory task with face stimuli.

During the resting-state period, participants were asked to lie still with their eyes open and look at a blank screen. The attention task (Fig. 1) required subjects to view sequences of visual stimuli on a screen, with the goal of detecting the presence or absence of a target stimulus in each of several test displays. Before each test display, subjects were presented with a cue arrow whose color and direction provided probabilistic information on whether and where the target stimulus might appear. The test display was then flashed for approximately 50 ms, after which the subjects were required to choose whether or not the target stimulus had appeared. In both memory tasks (Fig. 1), 180 previously studied stimuli and 180 novel stimuli were presented to the subjects, who were asked to determine whether each stimulus was “old” or “new”—i.e., whether it had been previously studied. As in the attention task, the memory tasks included probabilistic cues: each stimulus was shown either in a particular color (lexical stimuli) or bordered by a color (face stimuli) which provided subjects with the probability that the stimulus was novel. Face stimuli were drawn from a variety of online faces databases [24–29]. For additional experimental details, see [30], [31], and supplemental information therein.

Imaging

MRI data was acquired at the UCSB Brain Imaging Center from 116 healthy adult participants using a phased array 3T Siemens TIM Trio with a 12 channel head coil. Functional MRI data was taken while each participant engaged in the four tasks described above. This analysis combines two separate functional runs of the same attention task [30]. The sampling period (TR) was 2 s for the rest and attention tasks and 2.5 s for both memory tasks. In addition to functional data, a three dimensional high-resolution T1-weighted structural image of the whole brain was obtained for each participant.

Image Analysis

Structural MRI acquisition and pre-processing.

Structural scans were intensity-corrected, skull-stripped, normalized, segmented and parcellated (as described below) using FreeSurfer v.5.0.0 cortical reconstruction all with default settings,
accessed via the Connectome Mapping Toolkit v.1.2.0 [32]. The starting atlas was the updated Lausanne2008 multi-scale atlas [33]. For each subject, parcellations containing 83, 129, 234, 463 and 1015 regions were generated, covering cortical grey-matter regions, the thalamus, caudate, putamen, pallidum, accumbens area, hippocampus, amygdala and brainstem. The highest-resolution parcellation of 1015 regions was not investigated further, since a large number of regions contained very few or no voxels when the atlas was downsampled into fMRI space.

Functional MRI pre-processing and time series analysis. Preprocessing was performed using FSL v.5.0 [34–36], AFNI v. 2013.12.21 1014 http://afni.nimh.nih.gov [37] and Matlab (2013, The Mathworks, Natick, MA). Functional MRI scans were preprocessed as follows. FSL programs MCFLIRT [38] and fsl motion outliers were used to correct for head motion and derive a volume-by-volume measure of head motion: framewise displacement. Framewise displacement (FD) is calculated as the sum (in mm) of rotational and translational displacements from volume N to N+1 [39]. Next, we performed slice timing correction (AFNI 3dTshift), auto-masked to obtain a brain-only fMRI image (AFNI 3dAutomask), and smoothed the time series at each voxel (AFNI 3dDespike with default parameter settings). Despiking has been shown to reduce the motion-related distance dependent bias in correlation estimates [40]. Each voxel’s time series was then detrended with respect to framewise displacement using AFNI 3dDetrend. This uses linear regression to remove variability related to the nuisance regressor, framewise displacement, at each voxel. Runs were only included in the analysis if mean framewise displacement for the run was less than 0.25 mm per frame; this led to 73 fMRI runs (of 763 total runs) being excluded from this analysis. Registration proceeded as follows: a participant’s time-averaged fMRI image was aligned to their structural T1 scan using FSL FLIRT boundary-based registration [38,41], and the inverse of this transformation was applied to all subjects parcellation scales (generated in structural space). Parcellations were downsampled into EPI (AFNI 3dfrac- tionize, voxel centroid voting, requiring 60% overlap), and the mean signal across all the voxels within a given brain region was calculated to produce a single representative time series. The data was not spatially smoothed at any stage.

Creation of a hybrid atlas. We sought to create an atlas with low inter-individual and cross-brain variability in the amount of fMRI data acquired per region. Many existing atlases use parcellations that have roughly equal region sizes as measured on structural MRI scans [42]. However, down sampling the atlas from structural MRI voxels to fMRI voxels, along with inhomogeneous fMRI signal-loss, mean that this does not produce equally sized regions in functional MRI space. To mitigate this, we generated a ‘hybrid’ atlas by choosing those regions from various scales of the Lausanne2008 atlas that minimized cross-brain and intra-subject variability in region size. The intra-subject size variability was quantified by the coefficient of variation, defined for each region $i$ as $100\sigma_i/\mu_i$, where $\mu_i$ is the mean size of region $i$ over all subjects and $\sigma_i$ is the standard deviation. Starting with the scale 234 atlas, an iterative process was used to decrease intra- and intersubject variability in region size. Where a region had very few voxels (mean size < 25th percentile), or high variability in size across subjects (coefficient of variation > 30%), it was tentatively exchanged for a region from the next highest resolution atlas, effectively combining the initial region with other higher-resolution regions subsumed under the same anatomical heading. If this combination of regions decreased the inter-subject or within-subject variability in region size, the combined region was retained. If not, the initial poor quality region was rejected from the “hybrid atlas”. This was repeated until no further combinations of regions could decrease intra- and inter-subject variability while retaining neuroanatomically sensible groupings. Regions were excluded from the analysis altogether if there were fMRI runs in which no data was acquired in that region (frontal pole, entorhinal cortex and temporal pole), or if the inter-subject coefficient of variation was greater than 30% (this applied to 7 of the 8 inferior temporal regions; 1 of the 8 middle temporal regions; 2 of 8 fusiform regions; 1 of the 6 caudal middle frontal regions, and 1 of the 14 precentral regions). Table 1 lists the 194 regions identified by this hybrid atlas. This approach considerably reduced intra-subject variability in region size as well as reducing the inter-subject variability at problematic outlier regions, while minimizing the amount of data that had to be excluded from analysis.

Functional Connectivity

Specific frequencies of oscillations in the BOLD signal have been associated with different cognitive functions. We focus our investigation on low frequency (0.06–0.125 Hz) oscillations in the BOLD signal that have proven useful for examining resting [43,44] and task-based functional connectivity [18]. The task-related oscillations are posited to be specific to this frequency range, possibly due to a bandpass-filter-like effect from the hemodynamic response function [45]. We apply a Butterworth
Table 1. Brain regions.

| Region Name       | L | R |
|-------------------|---|---|
| lateralorbitofrontal | 2 | 2 |
| parsorbitals      | 1 | 1 |
| medialorbitofrontal | 1 | 1 |
| parstriangularis  | 1 | 1 |
| parsopercularis   | 2 | 2 |
| rostralmiddlefrontal | 5 | 6 |
| superiorfrontal   | 9 | 8 |
| caudalmiddlefrontal | 3 | 2 |
| precentral        | 7 | 6 |
| paracentral       | 1 | 1 |
| rostralantiorcingulate | 1 | 1 |
| caudalanteriorcingulate | 0 | 1 |
| posteriorcingulate | 2 | 2 |
| isthmuscingulate  | 1 | 1 |
| postcentral       | 7 | 5 |
| supramarginal     | 5 | 4 |
| superioparietal   | 7 | 7 |
| inferioparietal   | 5 | 6 |
| precuneus         | 5 | 5 |
| pericalcarine     | 1 | 1 |
| lateraloccipital  | 5 | 5 |
| lingual           | 2 | 3 |
| fusiform          | 3 | 3 |
| parahippocampal   | 1 | 1 |
| inferiortemporal  | 1 | 0 |
| middletemporal    | 3 | 4 |
| bankssts          | 1 | 1 |
| superiortemporal  | 5 | 5 |
| transverstemporal | 1 | 1 |
| insula            | 2 | 2 |
| thalamusproper    | 1 | 1 |
| caudate           | 1 | 1 |
| putamen           | 1 | 1 |
| pallidum          | 1 | 1 |
| accumbensarea     | 1 | 1 |
| hippocampus       | 1 | 1 |
| amygdala          | 1 | 1 |

Anatomical locations of the 194 brain regions used as network nodes in the hyperedge analysis, including the number of regions in left and right hemispheres in each brain area. doi:10.1371/journal.pcbi.1004029.t001

Time Windows for Temporal Network Construction

Dynamic networks are constructed by taking the filtered time series in temporal windows of 60 seconds and computing a $N \times N$ adjacency matrix of nodal correlations for each time window, where $N = 194$ is the number of nodes. Each of these $N \times N$ adjacency matrices represents the functional network over the 60 seconds in question. From this set of networks, we extract the edge weight time series by considering the correlation strength in each sequential network. We let $E = N(N−1)/2 = 18721$ be the total number of edges between the 194 nodes and construct an $E \times E$ adjacency matrix $X$, where $X_{ab}$ gives the Pearson correlation coefficient between the time series of edge weight for edges $a$ and $b$. The entries of the $E \times E$ adjacency matrix represent pairs of edges with correlated weight time series [23].

We consider a range of temporal window lengths from 40 to 120 seconds and find that our results for hyperedge size and spatial distributions are robust to changes in window length in this range. Because the TR varies between the memory tasks and the rest and attention tasks, windows of equal time length include different numbers of data points in different segments of the experiment. To ensure this does not affect our analysis, we conduct an analysis with the number of data points per window held constant, and obtain very similar results (see Figure 1 in S1 Text).

Hyperedge Construction

The cross-linked network structure, which contains information about groups of edges with similar time series (hyperedges), is extracted from the edge-edge correlation matrix $X$ [23]. Fig. 2 provides a schematic illustration of the process of determining the cross-linked structure of a network. To exclude entries of $X$ that are not statistically significant, we threshold $X$ by evaluating the $p$-values for the Pearson coefficient $R$ for each edge-edge correlation using a false discovery rate correction for false positives due to multiple comparisons [48]. If the $p$-value for an entry $X_{ij}$ satisfies the false discovery rate correction threshold, we set $\xi_{ij} = R(i,j)$ for our thresholded matrix $\xi$. We set the thresholded entry of all other elements $X_{ij}$ to zero. We binarize this thresholded matrix and obtain $\xi'_{ij}$, where

$$\xi'_{ij} = \begin{cases} 1, & \text{if } \xi_{ij} > 0; \\ 0, & \text{if } \xi_{ij} = 0. \end{cases}$$

Each connected component in $\xi$ represents a hyperedge, a set of edges that have significantly correlated temporal profiles. The groups of nodes in Fig. 2(D) are examples of such connected components. A single hyperedge may include any number of edges between one (a singleton) and numbers of data points in different segments of the experiment. To ensure this does not affect our analysis, we conduct an analysis with the number of data points per window held constant, and obtain very similar results (see Figure 1 in S1 Text).

This hypergraph technique builds on recent trends in the wider field of network science. First, identifying groups of network edges that share similar properties, rather than the groups of nodes that have traditionally been the focus of community detection methods, has been recently shown to provide more intuitive representations of overlapping nodal communities and hierarchical structure [49–51]. Second, the idea of identifying functional groups based on the temporal patterns of their interactions has proven useful [51,52]. Hypergraphs provide a straightforward method, both edge-based and intrinsically dynamic, of identifying and analyzing temporal patterns in network organization. In this work we focus on functional networks in the human brain, but the hypergraph-related diagnostics

bandpass filter to isolate frequencies in the (0.06–0.125 Hz) range [46].

To construct a functional brain network, we use the 194 region hybrid atlas, where each region contains a roughly equal number of voxels. These 194 regions represent the network nodes. The $x$, $y$, and $z$ positions of each node are given by the centroid of the voxels which comprise the node. Edge weights in the functional brain network are computed by taking Pearson’s correlations between the filtered time series within a defined time period for each pair of nodes [47].
introduced below are easily generalizable to a broad variety of dynamic networked systems.

**Hypergraph Diagnostics**

We use several methods to extract statistical features from individual hypergraphs and across the set of subjects.

**Hyperedge size.** We define the size, \( s(h) \), of a hyperedge \( h \), as the number of edges contained in it,

\[
s(h) = \sum_{i,j,k} \xi_{ijk},
\]

where the sum is performed over the upper triangular elements of \( \xi \), and \( \xi \) is the binarized edge-edge adjacency matrix defined above. Hyperedges with \( s(h) = 1 \) are singletons, which display no significant correlation between that edge and any other in the network. These singletons are excluded from further analyses. Additionally, we compute the cumulative hyperedge size distribution across all subjects in the study.

**Hyperedge node degree.** We define the hyperedge degree of a node to be the number of hyperedges that contain that node. We examine the hyperedge node degree distribution as a spatial distribution over the subjects as a group to understand characteristic hyperedge properties.

**Co-evolution network.** We construct a “co-evolution network” to consolidate hypergraph results into a single graph that illustrates where hyperedges are most likely to be physically located over an ensemble of individuals. Fig. 3 illustrates a schematic of our construction. We begin by defining the matrix, \( C \), of probabilities that edges are included in a hyperedge over a set of hypergraphs. Again, nodes correspond to brain regions and connections correspond to inter-region associations, but here the weight of a connection joining nodes \( i \) and \( j \) is the matrix entry \( C_{ij} \). The resulting static network encompasses the dynamics of hyperedge activity, with connection weight corresponding to the probability that the two nodes are co-evolving over all of the hypergraphs considered. In later sections, we refer to co-evolution connection “strength,” which we define as the magnitude of the probability matrix entry corresponding to that connection.

**Task-Specific Classification**

Previous work identified regions with task-specific activity in rest, attention, and memory tasks [30]. Further understanding of the regions that have a correlation structure unique to one task provides insight into network structure differences between tasks. To investigate the task-specific hyperedge structure, we first group hyperedges that exhibit a significantly higher correlation within one task into task-specific sets. If a hyperedge is significantly correlated in two or more tasks, it is excluded from the task-specific hypergraphs. The task-specificity of hyperedges is calculated by comparing the correlation within a single task to the correlation over the same time length with time points chosen randomly from other tasks. This permutation test uses a Bonferroni correction for false positives due to multiple comparisons [33]. Task-specific hypergraphs are then used to construct task-specific hyperedge size distributions, hyperedge node degree distributions, and co-evolution networks.

To quantitatively probe the differences in spatial organization of dynamic functional co-evolution networks for the four tasks, we investigate two summary metrics that show significant variation across tasks. Choice of these measures is primarily motivated by observed coarse differences in co-evolution network structure.

The first “length-strength” metric is the Pearson correlation coefficient, \( R \), between the strength of a connection in the co-evolution network and Cartesian distance between the two nodes linked by the connection (physical length). The Cartesian distance is computed by taking the \( x \), \( y \), and \( z \) coordinates of each node and calculating the square root of the differences squared. The length-strength metric identifies a geometric property of the network, as well as a coarse estimate of the length of the strongest connections. Furthermore, connection length is related to network efficiency [54,55], so differences in this measure could indicate varying levels of functional network efficiency corresponding to task states.

The second “position-strength” metric is the Pearson correlation coefficient, \( R \), between the strength of the co-evolution network connection with the average anterior-posterior position of the two nodes. A measure of anterior-posterior position for each connection was found by taking the average \( y \) position of the two nodes in the connection. Identifying the location of strong co-evolution network connections along the anterior-posterior \( y \) axis provides a measure of where hyperedges are physically present in task states. Both the structural core [33] and a dynamic functional core area, comprised of sensorimotor and visual processing areas [19], are located in the posterior, so nodes in these regions have negative \( y \) values. A larger negative position-strength value corresponds to a higher probability that hyperedges are active in these core areas.

The length-strength and position-strength metrics are evaluated for significance by comparing the correlation between length or position and connection strength to the same correlation performed on randomly chosen co-evolution connections. Again, the Bonferroni correction is performed to eliminate false positives due to multiple comparisons.

In Results, we discuss how these metrics reveal quantitative differences between task-specific networks. A more detailed analysis of the overlap between hyperedge co-evolution networks and relevant cognitive processing regions is also presented. In this analysis, we describe how delineated areas of higher hyperedge activity consistently correspond to recognized centers of task-specific activity.

**Null Models**

In this analysis, we compare our results with two statistical null models based on measures for dynamic networks [22]. Hyperedges are formed from correlated edge time series; consequently the null overall model randomly shuffles each edge time series over all experiments. This null model is designed to ensure that the hyperedges identified in our analysis can be attributed to the dynamics of the system, rather than some overall statistical property of the data set.

![Fig. 2. Hyperedge construction. A schematic illustration of the method used to identify hyperedges. We begin with a set of node-node edges (A) and their time series (B), of which three (green, pink and orange traces, (B)) exhibit strong pairwise temporal correlations. These edges are cross-linked (C) by temporal covariance in edge weight time series, and thereby form a hyperedge (D) of size three on six nodes. The final [blue] edge forms a singleton, an edge which is not significantly correlated with any other edges. doi:10.1371/journal.pcbi.1004029.g002](image-url)
The other null test we perform, which we will refer to as the null within-task model, reorders each edge time series within each task, keeping tasks distinct. This is constructed in order to determine whether there are specific differences in the data between tasks.

**Results**

We compile the results from the hypergraph analysis for each of the subjects and combine these results to obtain a size distribution, anatomical node degree distribution, and co-evolution network for the group. We then divide the data into task-specific hypergraphs and perform the previously mentioned analyses on the task-specific hypergraphs.

**Hypergraph Analysis and Statistics**

We construct a hypergraph for each individual and examine the cumulative distribution of hyperedge sizes \( s(h) \) from Equation 2, shown in Fig. 4. There is a distinct break in the slope between two branches of the distribution occurring at a size of approximately 100 edges, which we use to distinguish between “large” and “small” hyperedges. The total number of small hyperedges appears to roughly follow a power law with an exponent of approximately \(-2.5\). The number of large hyperedges peaks around the maximum size, with relatively few in the middle range from 100 to 1000 edges. In Fig. 4, the sharp drop off in the distribution at large hyperedge sizes reflects the system size limitation on hyperedge cardinality.

There is a distinct partition in all individual frequency versus sizes distributions; one or two “large” hyperedges \( s(h) > 100 \), and many “small” hyperedges \( s(h) < 100 \) that peak at the smallest size. A subject with relatively small maximum hyperedge size has hundreds of edges in this largest hyperedge, as well as multiple “small” hyperedges. The corresponding hypergraph of a subject with a maximum hyperedge near the system size is strongly dominated by the largest hyperedge, which contains almost all edges in the brain.

The null overall model shuffles the data over all tasks. There are no hyperedges greater than size one, so the results from this null model are not depicted in Fig. 4. These singletons signify no significant correlation with other edges. As a result, we performed no further analysis on this null model. The fact that no significant hyperedges were found in the null overall model validates the statistical significance of our results.

The null within-task model shuffles the data but ensures that task data stays within the same task. The size distribution of hyperedges from the null within-task model is shown in Fig. 4. The shape of the two distributions is similar, although the null within-task model has fewer hyperedges in the large regime and there are more singletons than in the original data. This indicates there is co-evolution structure across tasks because this structure corresponds to changes in edge states between two or more tasks. For example, if groups of edges have an overall high correlation in one task and a significantly lower correlation in another, it would induce a hyperedge across the tasks regardless of how the within-task time series are shuffled.

Examining the cumulative hyperedge size distribution provides information about the network topology but does not supply descriptive spatial information. Next, we quantify which anatomical locations in the brain participate in hyperedges, identifying differential roles in task-induced co-evolution. Fig. 5A depicts the hyperedge node degree on a natural log scale. The densest regions are located in posterior portions of the cortex, primarily in visual...
areas, while a second set of dense regions is located in the prefrontal cortex.

We construct a co-evolution network, as illustrated schematically in Fig. 3, where connection weight corresponds to the probability that two nodes participate in the same hyperedge. In Fig. 5B we present this co-evolution network over all individuals and all tasks. The graph includes sparse long-range connections between regions that are densely connected. Within the strongest 1% of connections, the high degree of bilateral symmetry indicates that corresponding nodes in the left and right hemispheres have a high likelihood of being placed together in a hyperedge. Dense areas of the graph include primary visual areas, portions of prefrontal cortex, and primary motor cortex.

**Task-Specific Hyperedges**

The hypergraph algorithm groups together edges with significantly similar temporal behavior. However, this basic classification does not distinguish whether the correlation is present throughout the edge time series, or whether highly correlated sections of the time series drive the selection. We compute the average within-task edge correlation for each hyperedge and find that in some cases, strong edge correlation spans the tasks, while in other hyperedges, a strong correlation between edges within one task drives the hyperedge. An example of this task-specific correlation structure can be seen in Fig. 6. In the average within-task correlation on the left, there is a stronger average correlation in the word memory task than in any other task. Furthermore, the edge time series in the first hyperedge indicates it is driven mainly by a correlation within the word memory task.

To investigate this further, we construct task-specific co-evolution networks, composed of hyperedges with significantly stronger average correlation in one task than the others (see Methods). To identify these task-specific hyperedges for each task, we perform a permutation test on the edge weight time series, as described in Methods, and compare the total correlation within the task to the expected values. If a hyperedge displays significant edge correlation (determined by the Bonferroni correction on the 

Fig. 4. Hyperedge size distribution. In the cumulative frequency distribution of hyperedge sizes, the small hyperedges appear to roughly follow a power law with an exponent of approximately −2.5, while the large group is concentrated near the maximum size. In the null overall model, there are no non-singleton hyperedges. Results for the null within-task model, where the data is shuffled within each task, are in green. doi:10.1371/journal.pcbi.1004029.g004

p-values from the permutation test in only one task, we label it as a task-specific hyperedge. Hyperedges with two or more tasks exhibiting significant correlation are not included in the task-specific hypergraphs.

Fig. 7 illustrates the size distributions of all the task-specific results alongside the overall hyperedge size distribution. The sizes and spatial distributions of single task-driven hyperedges vary across tasks and incorporate significant information about functional network organization with respect to changing cognitive states. Attention has the greatest number of task-specific hyperedges, followed by face memory, word memory, and rest. In the small regime, the tasks follow a similar distribution. There are fewer large attention and rest hyperedges, while the face memory task closely mimics the overall distribution. The distinction in the distributions indicates that the tasks can be characterized by differing complexities of edge co-variations.

The spatial distributions of hyperedge node degree in each task, along with task-specific co-evolution networks, are shown in Fig. 8. The rest hypergraph has the least activity in posterior regions of the cortex, both in the hyperedge node degree plot and co-evolution network. In the attention network, long connections connecting the front and back of the brain distinguish it from the rest network. Furthermore, the concentration in the occipital lobe is larger in the memory co-evolution networks than in the rest or attention networks. We characterize these observed differences
with two statistics, which are described in more detail in Methods. The length-strength metric is a correlation between connection length and strength in the co-evolution network. The position-strength metric is a correlation between connection position (anterior-posterior) and strength. The results of this analysis over the full unthresholded co-evolution network are in Fig. 9. All correlation values are negative, indicating that, in all tasks, stronger connections in the co-evolution network are located in posterior portions of cortex and are physically shorter.

We compare these values across tasks by performing pairwise permutation tests to determine which networks have statistically different properties. Fig. 9 depicts the \( p \)-values from these tests, where the horizontal axis represents the statistic being tested and the vertical axis corresponds to the task being tested against. The black squares in this figure represent significant values, which are summarized in the following list:

1. The rest task has a significantly less strong position-strength correlation than the word and face memory tasks. This confirms the observation that the rest co-evolution network is less likely than the memory networks to have strong connections in posterior regions of the cortex.
2. The attention task is less strongly correlated than the word memory task, as measured by the position-strength metric and the rest task in terms of the length-strength metric. Thus, the attention co-evolution network is less likely than word memory to have strong connections in the posterior, and less likely than the rest network to have strong connections that are short.
3. The word memory task has a weaker length-strength correlation than the rest and attention tasks. Thus, strong connections in the word memory co-evolution network are less likely be short than they are in attention and rest networks.

These results delineate significant differences in co-evolution network structure between the tasks, confirming that the hypergraph analysis is a useful method for distinguishing between task states. Additional features of the task-specific co-evolution networks are described in more detail below.

**Rest.** Rest-specific hyperedges are primarily represented in the “small” range of the size distribution in Fig. 7. Although it is difficult to distinguish in Fig. 7 due to the logarithmic scale, the rest task also has the lowest number of task-specific hyperedges. Consequently, its spatial hyperedge node degree distribution in Fig. 8A has the lowest overall magnitude across task states. The areas with the highest degree of hyperedge activity are in the posterior portions of the brain, a configuration that is consistent across tasks. This suggests there is an underlying pattern of hyperedge generation centered in the occipital lobe.

The rest-specific co-evolution network is highly clustered in the most probable 0.2% of co-evolution pairs, as visualized in Fig. 8B. High probability clusters occur in areas including the inferior parietal lobule, superior frontal gyrus, precuneus, and posterior cingulate cortex. Although the rest network displays clustering at
**Fig. 8. Task-specific co-evolution networks and hyperedge node degrees.** (A): Distribution of task-specific hyperedge node degree on the brain. Here, the log of the total number of hyperedges containing each node is represented on the brain. The color scale represents the log of hyperedge node degree as in 5A, although here the range of values is from 0 to 4.8. (B): Co-evolution networks for each task. Edge strength corresponds to the probability that a hyperedge will contain the edge over all individual hypergraphs. Color represents a threshold in percentage value, with the scale given in Fig. 5B, and the top 1% of co-evolution probabilities are shown. Once again, the top 2% of probabilities are brown, red indicates the top 0.2% to 0.4% of connections, orange indicates the top 0.4% to 0.6% of probabilities, gold indicates the top 0.6% to 0.8% of probabilities, and yellow indicates the top 0.8% to 1% of probabilities.

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**Fig. 9. Task-specific network statistics.** Values for the position-strength metric (blue) and the length-strength metric (red) for the four tasks are depicted in (A). (B) shows p-values for the pairwise statistical permutation test between tasks, where black denotes a significant value after a Bonferroni correction for multiple comparisons. Values are obtained for length-strength and position-strength metric. For example, on the y position plot in (B), attention-word is significant. Referring back to (A), we see that this implies the difference in the y position-strength correlation between the attention and word tasks is statistically significant.

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this highest threshold of probability, lower thresholds show very little structure; the top 1% of connections shown in Fig. 8B is far more randomized in rest than in the other task-specific co-evolution networks. There is relatively little lateral symmetry and few visible “core” areas with high hyperedge node degree.

The negative length-strength correlation for connections in the co-evolution network is significantly stronger for the rest task than the word memory task. This indicates that the strongest connections in the rest-specific co-evolution network are short, reflecting the initial observations in Fig. 8B. The rest co-evolution network also has the smallest negative correlation between connection position and strength, which the permutation test (Fig. 9B) confirmed to be significantly smaller than the word or face memory tasks. This means that the strongest rest-specific hyperedges are less likely to be located in the posterior of the brain than the strongest hyperedges specific to either memory task, a result again consistent with Fig. 3B.

**Attention.** Overall, there are more hyperedges associated with attention than any other task, although this is difficult to visualize in Fig. 5. The attention-specific hypergraph consists almost exclusively of small hyperedges. This lack of large hyperedges may account for the increased disorganization in the co-evolution structure at lower probability thresholds observed in both rest and attention co-evolution networks in Fig. 8B.

The spatial hyperedge node degree distribution for the attention task (Fig. 8A) appears qualitatively similar to the rest task, with a few areas of increased degree in the occipital lobe, and with overall larger hyperedge node degree values corresponding to the greater overall number of attention-specific hyperedges compared to rest.

The co-evolution structure specific to the attention task (Fig. 8B) has a higher degree of bilateral symmetry than the rest network, and has fewer strong connections in the occipital lobe than either memory task. There are multiple prefrontal cortical regions that are likely to cohesively evolve with several other nodes. Regions of high clustering in the most probable threshold include the lateral parietal and occipital lobes, the superior frontal cortex, and dorsal parietal cortex.

Numerous strong connections between rostral and causal brain regions are another feature of the attention-specific co-evolution network. The negative length-strength correlation in the attention co-evolution network is significantly less strong than in the rest task, consistent with the observation that the attention network has strong connections that reach across the brain (Fig. 8B). Additionally, the attention task has a significantly weaker position-strength correlation than the word memory task, likely driven by the strong attention co-evolution connections in the prefrontal cortex.

**Memory for words.** The word memory-specific hyperedge size distribution includes more large hyperedges than rest or attention, although it is not as close to the overall distribution as the face memory distribution.

The spatial hyperedge node degree distribution for the word memory task has high node degrees in similar brain areas to the other task-specific distributions. There is a marked increase in node degree of regions in the parietal lobe from rest and a decrease in degree of regions in the occipital lobe from attention (seen in Fig. 8A).

In the word memory co-evolution network in Fig. 8B, the strongest connections are highly clustered in the occipital or frontal lobes, with few connections to nodes in between, while the strength and number of bilateral links is diminished compared to the attention task. The negative length-strength correlation of connections in this network is the weakest for the word memory co-evolution network, and significantly weaker than in the rest or face memory tasks. As in the attention task, this is consistent with the many connections between the occipital and frontal lobes visible among the strongest links in the word memory co-evolution network (Fig. 8B).

**Memory for faces.** There are more large hyperedges significantly correlated in the face memory task than any other task-specific group. The task-specific size distribution closely resembles the overall distribution in the large regime, indicating that a significant portion of all large hyperedges are driven by correlations in the face memory task.

The face memory-specific hyperedge node degree values are consistently the largest across the brain. This is primarily due to the many large hyperedges specific to the face memory recognition task. In the word memory and attention degree distributions, there are areas of higher hyperedge node degree in the parietal lobe and occipital lobe, respectively, but the face memory degree distribution is more evenly dispersed over the brain.

The structure of the face memory-specific co-evolution network, shown in Fig. 8B, is most dense in the occipital lobe, consistent with the visual nature of the task. There are several strong connections from the occipital lobe to other brain regions, specifically in the prefrontal cortex and frontal lobe. While the structure looks similar to that of the word memory co-evolution network, the strong cluster of face memory co-evolution connections in the occipital lobe has fewer strong connections and less nodes involved overall than the corresponding word memory co-evolution network cluster, but more strong connections to a few particular nodes. Compared to word memory, the face memory-specific network also displays fewer strong connections in the frontal lobe but more strong connections among regions in the dorsal attention network. In addition to the properties discussed in previous sections, the face memory co-evolution network has a strong negative position-strength correlation, indicating that the strongest connections tend to be in the posterior of the brain.

**Discussion.**

Progress in understanding functional brain network topology provides significant insight into broad neuroscience questions regarding the brain’s organization and ability to effectively transition between cognitive states. Quantifying complex network dynamics in the brain will further understanding in these areas and has promising applications to behavioral adaptation and learning [18,19,21]. We apply hypergraph analysis, a tool from dynamic network science, to functional brain imaging data in order to determine co-evolution properties of the brain as subjects perform a series of tasks. A previous application of this method to neuroscience uses hypergraphs to analyze how functional network structure changes over a long term learning task [19]. The learning experiment considers hypergraphs constructed over 6 weeks of training while subjects acquire a new motor skill, while our analysis compares hypergraphs over three different tasks performed within an interval of hours. Our analysis shows that hypergraphs are a useful tool for investigating shorter time scales and differentiating between task-specific networks.

Instead of analyzing the time-dependent behavior of groups of nodes, the hypergraph investigation considers the edge weight time series, where edges with statistically significant similarities in their temporal profiles are grouped into hyperedges. This approach is advantageous because it considers all edges, regardless of correlation strength, unlike previous methods which focus exclusively on strong correlations [30,56]. The use of a data-driven analysis also allows us to investigate the dynamic changes in brain function over a series of tasks without prior assumptions of the
structure of the connectivity network. This is a significant advantage over methods that characterize task states based on their differences with respect to the rest network [3,4]. A comparison between the hypergraph analysis and these methods in a future analysis could reveal how the concentration of hyperedges varies in known task-positive or task-negative areas and determine whether this variation has an effect on task performance.

Hypergraph Statistics and Structural Metrics

We demonstrate the existence of hypergraph structure in functional brain dynamics and statistically characterize the hyperedge distributions in comparison to appropriate null models. Shuffling the time series over all time produces no significant hyperedges, while shuffling within each task results in a size distribution that resembles the overall size statistics in shape, but with far fewer hyperedges. The distinct differences between the two null models and our results based on the original time series establish the significance of our findings. Furthermore, the existence of hyperedges after the within-task shuffling indicates the presence of activity in some edges that is differentiated between tasks. Since there are fewer large hyperedges after the within-task shuffling, we can also confirm that there are hyperedges caused by edge dynamics within tasks. This work primarily concentrates on hyperedges correlated within a particular task, but future analyses to understand the properties of hyperedges that are grouped due to other general properties would supplement our results.

The hyperedge size distribution is comprised of “small” and “large” hyperedges, where the size distribution of the small hyperedges follows a power law and the large hyperedges peak at the system size. We explore the overall spatial hyperedge distribution by constructing a hyperedge node degree plot, and find that the majority of the most densely connected nodes lie in the posterior portions of the brain. To better observe spatial hyperedge properties, we develop a co-evolution network, where connection weights correspond to the probability that a hyperedge will include the connection. The top 1% of connections in the network with the highest probability of inclusion in a hyperedge are most concentrated in the occipital lobe and prefrontal cortex. These are expected areas of hyperedge concentration, consistent with the visual nature of the tasks, as well as the coordination of quick decision making and the selection of specific motor responses.

Task-Specificity and Anatomical Placement

We find there are hyperedges that are more correlated in one task and hyperedges that have a distinct profile across the tasks. Our results suggest that edges with a high probability of inclusion in task-specific hyperedges are often found in previously identified brain areas associated with the corresponding tasks, as discussed in detail below, confirming that the approach captures relevant information about task networks. In some cases, brain regions expected to show strong co-variation in a certain task are not included among the strongest connections of that task-specific co-evolution network; we also discuss examples of this in detail below. Repeating the analysis and grouping hyperedges that are significantly correlated in two tasks might lend insight into whether brain systems relevant to a certain task contain hyperedges that are correlated in another task and thus are rejected from our task-specific analysis.

In all tasks, stronger connections in the co-evolution network tend to be located in posterior portions of cortex and to be physically shorter. The higher probability of posterior edges to be included in hyperedges is consistent with the identification of a core set of highly structurally connected regions centered in the posterior of the brain, thought to play an important role in integrating large-scale functional connectivity [19,33]. The tendency of strong connections to be physically shorter suggests high efficiency in task-specific co-evolution networks. This may reflect efficient wiring properties associated with minimal wiring for rapid processing and low energy expenditures found in structural brain networks and shared by some other biological and technological networked systems [37].

Rest. Resting-state brain activity contains correlated patterns that comprise a default mode network, a system that is engaged during internal cognition [58,59]. Certain brain regions active at rest are consistently deactivated during goal-oriented tasks, indicating that they comprise a functional mode that is rest-specific [1].

Our result that rest has fewer specific hyperedges than the attention or memory tasks could be a result of the specificity of correlated resting state regions, or a simplicity intrinsic to resting state function that does not necessitate more concerted efforts involving numerous brain regions [11]. In addition, we see a relative randomization and asymmetry in the spatial co-evolution distribution of rest-specific hyperedges, as well as a relative lack of long, strong connections; these results may correspond to a diminished need for efficient processing in a task-free environment.

Dense areas of the co-evolution network with high probabilities of being in rest-specific hyperedges include brain regions traditionally associated with the resting state. The inferior parietal lobule, superior frontal gyrus, precuneus, and posterior cingulate cortex have been identified as integral components of the default mode network; in addition, the posteromedial cortex, which includes the precuneus and posterior cingulate cortex, plays an important role in awareness [60–62].

Attention. Two attention systems exist in the human brain: a “top-down” network controls goal-directed attention, while a “bottom-up” group of brain regions detects and orients attention to relevant sensory stimuli that are generally novel or unexpected [63, 64]. Our task probes the former, as subjects are asked to focus on repetitive stimuli in a controlled environment. This requires an “executive control network,” a bilateral dorsal system that governs guided attention and working memory [65]. The relatively high degree of bilateral symmetry and the dorsal concentration of connections observed in the attention-specific co-evolution network suggests a higher probability for connections within this executive control network to co-evolve with other edges during the attention task.

Specifically, we observe regions of high clustering among the strongest connections in the attention-specific co-evolution network in the lateral parietal and occipital lobes, superior frontal cortex, and dorsal parietal cortex, areas known to be involved in attention networks. Parietal and frontal areas are involved in attention control and localization, specifically in visual attention tasks [63,66]. Activation of the superior frontal cortex occurs in attention tasks, especially those that involve a shift to peripheral locations in the visual field [67,68]. The dorsal parietal cortex also performs a central role in the executive control network: patients with lesions in the dorsal parietal cortex have shown significant impairment in goal-directed attention tasks [69].

Strong connections in the attention co-evolution network are more likely to be long than those in rest, corresponding to the high probability that long rostral-caudal edges will be included in hyperedges (visible in Fig. 8B). This may reflect a greater need for coordination between prefrontal executive control regions and regions in the occipital lobe during the attention task. In addition,
strong attention-specific co-evolution connections are less likely to be located in the posterior of the brain than those specific to word memory; this could indicate that the attention task state has less reliance on core visual regions than the word memory task state.

**Memory for words.** Our results for the word memory-specific and the face memory-specific hypergraphs were similar in several ways. Both displayed many more “large” hyperedges than the rest or attention tasks, suggesting that some aspect of the memory tasks requires dynamically coherent evolution over much of the brain. We speculate that this variation in the task-specific size distributions may correspond to the cognitive complexity demanded by the tasks, with the more involved memory tasks requiring more coordination between different cognitive networks and functions, and therefore producing more large hyperedges. This possibility could be further tested by examining hyperedge size variation across tasks specifically designed to vary in complexity.

Visual orthographic and face processing have a common reliance on central vision [70] and share neural circuitry [71]. The resemblance of the co-evolution networks for the two tasks, especially when compared with the very different graph structure of the attention and rest networks, indicates a similarity in the hypergraph representation of the memory tasks. This in turn signifies a correspondence in brain dynamics specific to memory. The task-specific analysis identifies hyperedges that show a significant correlation in only one task, so there is no overlap in these co-evolution networks.

Existence of a dedicated visual word processing network has been a topic of frequent discussion in neuroscience. The visual word form area (vWFA), located in the occipito-temporal cortex, is consistently activated by orthographic stimuli [72] and is invariant to changes in case, size, font, or type of visual stimulation [73,74]. The vWFA has also been shown as functionally linked to the dorsal attention network in resting state fMRI data, indicating that it fulfills a complex cognitive role [75].

In the word memory-specific co-evolution network, the vWFA is highly connected, but there is minimal strong structure in dorsal attention areas, which we would expect to see in a functional connectivity analysis [75]. This can be explained by our methodology of selecting task-specific hyperedges. If edges in the dorsal attention network have similar co-evolution properties within the word memory and attention tasks, they will not be identified as task-specific edges.

**Memory for faces.** Face recognition in humans requires a complex network distributed throughout the visual cortex that includes extended connections branching to other cortical regions [76]. The majority of visual processing occurs in the occipital lobe, located in the posterior of the brain. Functional MRI studies have identified multiple regions in the occipital cortex that respond more strongly to faces than other visual stimuli, indicating that the cognitive processes involving facial recognition are highly specialized [77,78]. The especially dense concentration of connections in the occipital lobe at the highest probability levels of the face memory-specific co-evolution network is consistent with this.

The face perception system is composed of multiple bilateral regions; the lateral symmetry observed in the face memory-specific co-evolution network is consistent with this structure [76]. An aspect of the co-evolution network that breaks this symmetry is the right fusiform gyrus, which is strongly connected to other areas in the occipital lobe by high probability co-evolution pairs. A region in the fusiform gyrus, the fusiform face area (FFA), has been found to be selectively active in whole human facial perception, and the right FFA in particular has been found to have the most salient response to faces, with damage to the region severely impairing face recognition [79,80]. The high probability of co-evolution between the right fusiform gyrus and other regions in this task-specific hypergraph is consistent with our expectation that regions involved in the memory of faces in particular (as opposed to words) are most likely to be included in face memory-specific hyperedges.

The co-evolution networks for both memory tasks show a significantly higher hyperedge probability in visual areas than the attention and rest tasks, and the differences in structure indicate that the hypergraph representation of memory tasks is significantly different from rest or attention. The marked differences in hyperedge statistics between task states in our task-specific analysis suggest hypergraphs as a measure of functional network changes due to task states. With measures derived from the hyperedge analysis, we can begin to quantitatively probe the mechanisms of functional switching between tasks and gain insight into how distinct features of the network evolve in synchronized patterns.

**Methodological Considerations**

Because they consider both strong and weak edges with no thresholding, hypergraphs are well-suited for identifying groups of brain regions that, for example, initially have uncorrelated activity but become more correlated in synchrony (or vice-versa), as we expect task-associated cognitive networks to do as a result of switching between tasks. In order to extract these dynamic patterns, the hypergraph technique considers strong and weak edges equally, ignoring any offset between the average correlation strengths of different edge time series. This is intended to provide a complementary method to the common thresholding approach of separating or ignoring network edges with correlation strengths weaker than some critical value [30,56]. Since weak edge connectivity has been shown to contain functionally relevant and predictive information in various contexts, retaining these edge weights is desirable [44,81,82]. There is also evidence that mean edge correlation values can be driven by non-biological artifacts such as head motion, even after applying standard motion-correction techniques [20]; by remaining indifferent to edge weight offsets, a hypergraph analysis avoids this concern.

In applications where the overall correlation strength of network edges is nevertheless important, it may be useful to supplement the dynamic information given by a hypergraph analysis with a measure that retains this edge weight information. Efforts to make quantitative comparisons between the hypergraph analysis and other dynamic graph theoretical methods in the context of the human brain are ongoing. We are currently investigating whether dynamic community detection on weighted brain networks, a node-based analysis which relies on edge correlation strength, provides complementary information to the hypergraph analysis.

Because we choose a linear measure to compute correlations between edge weight time series, our analysis as presented here does not account for time lag in these correlations. However, our framework could be extended to nonlinear measures that include time-lag information.

It is important to note that our method of computing a dense matrix of edge-edge correlations and thresholding according to significance does not necessarily identify direct conditionally-dependent correlations between time series, or correlations that represent the underlying structural connectivity of the brain. As with any method that infers a network structure from correlation data simply by thresholding, we expect many of these correlations to be indirect. For example, a significant correlation between two edge weight time series may occur because both edges are being controlled by a third, more central edge – and not because the two edges are directly connected either causally or structurally. In this sense, the edge-edge correlation structure does not capture
relations that necessarily reflect the underlying control structure or the physical architecture of the brain. Our hyperedge analysis moves the focus away from such indeterminate dyadic relationships, considering only groups of all edges that share similar dynamic patterns without any intra-group organization or structure.

It is also possible, as in any fMRI analysis, that edge-edge correlations arise from task-induced indirect drivers, such as visual stimuli. Two regions that are both activated by a visual stimulus may show strong functional connectivity with one another in a single time window. Moreover, such regions may show similar changes in functional connectivity over time if their activation profiles to the stimulus evolve similarly during the experiment. As with any measurement of functional connectivity based on the Pearson correlation coefficient [33], a common and robust measurement of functional connectivity, such indirect drivers of functional connectivity are not distinguished from other more direct drivers of communication or interaction.

Throughout this work, we observe a significant amount of individual variability in the hypergraph properties of interest. In this manuscript, we have completed a group-level analysis and focused on investigating task-related differences in hypergraph structure. However, individual variability may be related to differences in cognitive ability and provide additional insight into the role of hyperedges in task performance, which is a topic of future research.

Final Remarks

In this paper, we use hypergraph analysis to identify significant co-evolution between brain regions in task-based functional activity and develop new tools to summarize the spatial patterns of these co-evolution dynamics over the group of subjects. By isolating task-specific hyperedges, we quantify significant differences between the spatial organization of co-evolution dynamics within different tasks. This hypergraph analysis adds a crucial perspective to previous treatments of task-based brain function, describing temporal similarities between spatially segregated neural circuits by specifically examining the organization of connections that co-evolve in time. It provides a promising approach for understanding fundamental properties of task-based functional brain dynamics, and how individual variation in these properties may correspond to differences in behavior and task performance.

Supporting Information

S1 Text Supplementary methodological information.

Discussion of the effects of time window selection and brain region size on the results, with accompanying figures. (PDF)

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Author Contributions

Conceived and designed the experiments: END KJS DSB MEL MBM STG JMC. Performed the experiments: END KJS DSB MEL MBM STG JMC. Analyzed the data: END KJS DSB MEL MBM STG JMC. Contributed reagents/materials/analysis tools: END KJS DSB MEL MBM STG JMC. Wrote the paper: END KJS DSB MEL MBM STG JMC.

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