Original Research

Application of intraoperative electrocorticography in bypass surgery for adult moyamoya disease: a preliminary study

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Abstract

Objective: Postoperative complications of surgical revascularization in moyamoya disease (MMD) are difficult to predict because of poor knowledge of the underlying pathophysiological process. Since the aim of surgery is to improve brain dynamics by increasing regional blood flow, we hypothesize that postoperative complications are closely related to aberrant electrophysiological changes. Thus, we evaluated the clinical significance of intraoperative electrocorticography (iECoG) in bypass surgery for adult MMD. Methods: Ninety-one adult patients operated on by the same neurosurgeon in our institute were involved (26 in the iECoG group, 65 in the traditional group). Two 1 × 6 subdural electrode grids were placed parallel to the middle frontal gyrus and superior temporal gyrus to record ECoG data continuously during the procedure in the iECoG group. Selected from several M4 candidate arteries, the recipient artery was determined to be closer to the cortex with lower power spectral density (PSD) in the beta band. The PSD parameter we used was the (delta+theta)/(alpha+beta) (DTABR) ratio (DTABR). Next, the pre- and post-bypass PSD values were evaluated, and correlations between post-/pre-bypass PSD parameter ratios and neurological/neuropsychological performance (in terms of changes in National Institutes of Health Stroke Scale [NIHSS] and Mini-Mental State Examination [MMSE] scores) were analyzed. Results: Postoperative complications (transient neurological events) in the iECoG group were significantly lower than those in the traditional group (p = 0.046). In the iECoG group, the post-/pre-bypass DTABR ratio in the bypass area was significantly correlated with postoperative NIHSS (p = 0.002, r² = 0.338) and MMSE changes (p = 0.007, r² = 0.266). In the nonbypass area, neither postoperative NIHSS nor MMSE changes showed a significant correlation with the post-/pre-bypass DTABR ratio (p > 0.05). Additionally, patients with postoperative complications exhibited significantly higher DTABR (1.67 ± 0.33 vs. 0.95 ± 0.08, p = 0.003) and PSD of the theta band (1.54 ± 0.21 vs. 1.13 ± 0.08, p = 0.036). Conclusions: This study is the first to explain and guide surgical revascularization from the perspective of electrophysiology. Intraoperative ECoG is not only sensitive in reflecting and predicting postoperative neurological and cognitive performance but also usable as a reference for recipient artery selection.

Keywords: Moyamoya disease; iECoG; Cognitive function; Bypass surgery

2. Introduction

Moyamoya disease (MMD) is characterized by progressive stenosis or occlusion of the distal internal carotid artery or proximal middle cerebral artery, and it leads to the formation of abnormal collateral vessels at the base of the brain. Surgical revascularization, including direct, indirect, and combined bypass, has been confirmed to benefit MMD patients with both ischemic and hemorrhagic stroke episodes [1]. Nevertheless, postoperative complications such as cerebral ischemia, epilepsy, and hyperperfusion syndrome, have been increasingly reported [2,3]. These complications may prolong hospitalization and be irreversible but can hardly be predicted by our present knowledge and experience [4].

Electroencephalography (EEG) has a high temporal resolution and is therefore suited to evaluating variations in neural activity after an event [5]. Previous studies have shown that alpha power reduction in continuous quantitative EEG predicts delayed cerebral ischemia, reflects successful therapy and predicts good functional outcome after subarachnoid hemorrhage [6,7]. Based on these findings, several studies indicate that EEG can promptly detect cerebral responses to successful reperfusion therapy [8]. Intraoperative electrocorticography (iECoG) is a newly developed method that combines EEG recordings with plastic surgery and allows for continuous monitoring of electrical activity during surgery [9]. This technique has already been used in MMD surgery to predict postoperative complications and guide surgical planning [10]. However, the clinical significance of iECoG in the preoperative selection of recipient arterial pathways in MMD surgery remains unclear.
oped EEG monitoring method with a higher sensitivity and accuracy and has been widely used in neurosurgery to help distinguish high-frequency oscillations continuously and noninvasively [9]. Its indices, such as relative delta power, delta/alpha power ratio (DAR), and delta+theta/alpha+beta power ratio (DTABR), are associated with ischemic lesions [10]. Finnigan et al. [11,12] believed that the delta/alpha power ratio (DAR) demonstrated maximal accuracy for discriminating between acute ischemic stroke patients and controls.

Currently, successful bypass surgery is still evaluated by the patency of anastomosis rather than the rate of postoperative complications. It’s vital for us to realize that effectiveness of bypass is based not only on hemodynamic remodeling, but on functional re-plasticity as well. Clinical experience indicates that patent anastomosis and sound clinical outcomes cannot always be achieved simultaneously. Poor knowledge of neural interactions before and after surgical revascularization may be the main reason. Thus, the present study evaluated the application of iECoG in adult MMD and tried to explore the effectiveness of bypass surgery from the perspective of electrophysiology.

3. Methods

3.1 Patients

All patients with MMD who were admitted to our hospital between May and August 2018 were consecutively enrolled in this study. Our study used historical controls that included 65 hemispheres in 65 patients who received the same operation without iECoG monitoring between January and May 2018. Inclusion criteria were (1) a Chinese population aged 18–65; (2) no evidence of infarction history, but small patches of hyperintense signal that were neither larger than the arbitrary cutoff of 8 mm in maximum dimension on T2-weighted MR images nor cystic in neither larger than the arbitrary cutoff of 8 mm in maximum dimension on T2-weighted MR images nor cystic in the cerebral subcortical white matter; (3) diagnosis through digital subtraction angiography; (4) no surgery before recruitment; (5) physically capable of cognitive evaluation; (6) meet the surgical indications of guidelines for MMD [4] and (7) absence of significant psychiatric disorders or neurological diseases that could compromise cognition. Patients with severe systemic or other cerebrovascular diseases and those taking drugs were excluded.

All patients underwent a combined revascularization procedure in which the superficial temporal artery was anastomosed to the M4 portion (cortical segment) of the middle cerebral artery near the Sylvian fissure and encephaloduromyosynangiosis (EDMS) surgery. The patency of the bypass artery was confirmed using indocyanine green (ICG) angiography. We used intraoperative cortical electrodes for electrophysiological monitoring, and the power spectral density (PSD) of each frequency band was calculated in real time. When selecting the recipient artery out of the two or more candidate arteries, we selected the artery closer to the cortex with lower PSD in the high-frequency bands according to the iECoG recordings and real-time PSD calculation. During the direct revascularization procedure, iECoG data were recorded continuously until the dura incision. The study protocol was approved by the ethics committee of Huashan Hospital, China, and all subjects provided informed consent (Fig. 1).

3.2 Clinical assessment

Baseline examinations involved taking a medical history and carrying out a physical examination. Neurological deficits and cognitive performance were quantified using the National Institutes of Health Stroke Scale (NIHSS) and Mini-Mental State Examination (MMSE) at arrival at the neurosurgery department and at 1 month after anastomosis. Perioperative complications, including cerebral hemorrhage, cerebral infarction, epilepsy and transient neurological events (TNEs), were confirmed by imaging examination and nervous system physical examination.

3.3 iECoG recordings

All patients received inhalation anesthesia administered by anesthesiologists, with end-tidal sevoflurane maintained at 2% during the iECoG recording. The iECoG data were recorded with a BrainAmp MR PLUS (Brainproduct, Munich, Germany) using a preamplifier bandwidth of 0.5–250 Hz and a sampling rate of 500 Hz. Two 1 × 6 subdural electrode grids were placed in parallel on the cortex intraoperatively. These electrodes were positioned on the middle frontal gyrus and superior temporal gyrus around the donor artery, and placement was confirmed using a neuronavigation system (Brainlab neuronavigation, Munich, Germany). The reference and earth electrodes were placed on the scalp. iECoG data were recorded continuously until dura closure.

3.4 PSD analysis

We selected the three electrodes from the two 1 × 6 electrode grids that were closest to the bypass site, and the mean PSD was calculated. The mean PSD of three non-bypass site electrodes was also calculated. PSD was calculated by fast Fourier transform over the range 1–60 Hz using MATLAB (MathWorks, Natick, MA, USA). PSD is the frequency response of a random or periodic signal. This tells us where the average power is distributed as a function of frequency.

The PSD is deterministic, and for certain types of random signals, it is independent of time. This is useful because the Fourier transform of a random time signal is itself random and therefore of little use in calculating transfer relationships (i.e., finding the output of a filter when the input is random). The PSD of a random time signal x(t) can be expressed in one of two ways that are equivalent to each other.
Fig. 1. ICG and iECoG monitoring for modified revascularization. The diagnosis of moyamoya disease (MMD) was confirmed by digital subtraction angiography (DSA) (A,B). Two 1 × 6 grids of electrodes were placed on the cortex close to the anastomosis site (C). The patency of the bypass artery was confirmed using intraoperative fluorescein angiography (D). Real-time ECoG monitoring during surgery (E).

(1) The PSD is the average of the Fourier transform magnitude squared over a large time interval.

\[ S_x(f) = \lim_{T \to \infty} E \left\{ \frac{1}{2T} \left| \int_{-T}^{T} x(t) e^{-j2\pi ft} dt \right|^2 \right\} \]

(2) The PSD is the Fourier transform of the autocorrelation function.

\[ S_x(f) = \int_{-T}^{T} R_x(\tau) e^{-j2\pi ft} d\tau \]
\[ R_x(\tau) = E \{ x(t) x^*(t + \tau) \} \]

The power can be calculated from a random signal over a given band of frequencies as follows:

(1) Total Power in x(t):

\[ P = \int_{-\infty}^{\infty} S_x(f) df = R_x(0) \]

(2) Power in x(t) in the range f1–f2:

\[ P_{f2} = \int_{f_1}^{f_2} S_x(f) df = R_x(0) \]

Data in this study were derived from the mean values of the three electrodes in the bypass area and the three in the nonbypass area. For each electrode over the range of 1–30 Hz, the power of the delta (1–3 Hz), theta (4–7 Hz), alpha (8–13 Hz) and beta1 (14–20 Hz) frequency bands over all channels were used to calculate the global DTABR.

Once the electrode grids were placed on the cortex, data were recorded and labeled as “Pre”. After the anastomosis was finished and temporary blocking clips of recipient artery were removed, data were labeled as “Post”. A period of interference-free waves was picked out for each period and pre- and post-bypass PSD were analyzed separately. Artifacts caused by electronic devices and motion were removed from the raw ECoG data by two neurosurgeons. We first compared the PSD of patients between pre- and post-bypass phases in the bypass area. To compare the spectral power of each band, the ratio of the spectral power of each band to that of the whole was calculated as follows: \( X/\text{DTAB} = \) (spectral power of each band)/(sum of spectral power of 4 bands: delta, theta, alpha, beta), where X is the spectral power of the delta, theta, alpha or beta band.

For both the bypass and nonbypass areas, we then compared the PSD for each frequency band and the DTABR between the pre- and post-bypass phases. To detect the changes in each parameter before and after surgery, the ratios between postoperative and preoperative values were used.
### Table 1. Baseline demographics in different groups.

| Characteristics | iECoG group | Control group | p value |
|-----------------|-------------|---------------|---------|
| Number          | 26          | 65            |         |
| Age             | 45.38 ± 9.05| 45.18 ± 11.27 | 0.94    |
| Sex (Male)      | 12          | 30            | 0.569   |
| Perioperative complications |       |               |         |
| Hemorrhage      | 0           | 1             | 0.714   |
| CI              | 1           | 2             | 0.64    |
| EP              | 3           | 7             | 0.916   |
| TNEs            | 1           | 13            | 0.046*  |
| Total           | 5 (19.2%)   | 23 (35.3%)    | 0.103   |
| Baseline NIHSS  | 1.615 ± 0.2081 | 1.769 ± 0.268 | 0.731   |
| ∆NIHSS          | -0.077 ± 0.293 | -0.3078 ± 0.168 | 0.478  |
| Baseline MMSE   | 24.04 ± 0.357 | 23.58 ± 0.269 | 0.349   |
| ∆MMSE           | 0.539 ± 0.243 | 0.785 ± 0.241 | 0.5523  |

CI, cerebral infarction; EP, epilepsy; TNEs, transient neurological events; NIHSS, National Institutes of Health Stroke Scale; MMSE, Mini-Mental State Examination.

### 3.5 Data analysis

The incidences of perioperative complications (cerebral infarction, epilepsy, and cerebral hyperperfusion syndrome) were compared between the two groups (MMD patients who received bypass surgery with and without iECoG monitoring). Data were compared between the two groups using the \( \chi^2 \) or unpaired \( t \) test, as appropriate. To determine the effect of various parameters on perioperative complications, logistic regression analysis was conducted using parameters with \( p < 0.05 \) in the univariate analyses.

### 4. Results

#### 4.1 Demographics

A total of 26 patients with MMD were examined. The mean age of these patients was 45.38 ± 9.25 years (range 28–61 years). All surgeries were performed by the same neurosurgeon (YX Gu), and their baseline characteristics are presented in Table 1. Continuous iECoG monitoring was conducted during the bypass surgery. The overall postoperative complication rate of patients receiving bypass surgery under the guidance of electrophysiological monitoring was lower than that of the traditional group, but the difference was not statistically significant (19.2% vs. 35.4%, \( p = 0.131 \)); however, the incidence of TNEs was significantly lower than that of the traditional group (3.8% vs. 20%, \( p = 0.028 \)).

#### 4.2 PSD analysis

##### 4.2.1 Bypass area

The mean values of PSD in the pre- vs. post-bypass phases in the bypass area were as follows: D/DTABG, 0.10 ± 0.063 vs. 0.11 ± 0.062. In most cases, high-frequency band PSD increased after bypass surgery, but no significant difference was found.

Fig. 2 shows the correlations between the post-/pre-bypass PSD parameter ratios for each frequency band and the change in NIHSS score. The post-/pre-bypass DTABR was significantly correlated with the change in the NIHSS score (\( p = 0.002, r^2 = 0.338 \)). No significant correlation was found between the post-/pre-bypass PSD ratios and the change in the NIHSS score.

Fig. 3 shows the correlations between the post-/pre-bypass PSD parameter ratios for each frequency band and the change in cognitive performance, as assessed by MMSE scores. The post-/pre-bypass DTABR decreased as the MMSE score increased (\( p = 0.007, r^2 = 0.266 \)). No significant correlations between the post-/pre-bypass PSD ratios and the change in the MMSE score were found.

##### 4.2.2 Non-bypass area

We also analyzed correlations between the post-/pre-bypass PSD parameter ratios for each frequency band in the nonbypass area and changes in neurological and cognitive performance. Neither the NIHSS nor the MMSE score was correlated with indices of intraoperative cortical electrophysiology (Figs. 4, 5).

#### 4.2.3 Complications analysis

We further compared the post-/pre-PSDs and DTABR ratio among patients with and without postoperative complications. In the bypass area, the DTABR ratio (1.67 ± 0.33 vs. 1.04 ± 0.10, \( p = 0.045 \)) and PSD of the theta band (1.54 ± 0.21 vs. 1.13 ± 0.08, \( p = 0.036 \)) were significantly higher in patients with postoperative complications. In the nonbypass area, no significant difference was found.
between the two groups in the post-/pre-PSD and DTABR ratios (Figs. 6, 7).

5. Discussion

Our results quantitatively confirm previous findings in which the PSD of the $\alpha$ and $\beta$ bands increased after anastomosis in MMD patients [13]. For the first time, the DTABR after bypass surgery was found to be correlated with neurological outcomes of MMD, and it may serve as a predictor of patient outcomes. For the first time, iECoG was applied to select recipient vasculature in bypass surgery for MMD and has been proven to effectively reduce the occurrence of postoperative TNEs in our study.

5.1 Postoperative PSD changes in different frequency bands

In line with previous studies [14–18], our results demonstrated that the PSD of high-frequency waves increased, while the PSDs of the low-frequency bands were
Fig. 3. Correlations between the post-/pre-bypass PSD and DTABR ratios for the bypass area and MMSE score change. PSD, power spectral density; DTABR, (delta+theta)/(alpha+beta) ratio; MMSE, Mini-Mental State Examination.

The process of revascularization is rapid, occurring within a few minutes to a few days [19–21]. Zhang et al. [4] have confirmed the clinical significance of hemodynamic parameters change in bypass surgery to predict perioperative complications, which has a high spatial resolution. While, neural electrophysiological monitoring can reflect changes in cerebral blood flow and metabolism within seconds, as these factors are directly reflected in neuronal rhythms with high temporal resolution [22]. The high temporal resolution of EEG permits sensitive assessment of instantaneous brain functioning [23,24]. EEG spectrum frequencies associated with acute cerebral ischemia have been discussed [11,17], but there are few reports on QEEG characteristics related to bypass surgery.

Interestingly, in our study, not all cases showed an attenuated after bypass surgery. This provides new evidence for the physiological significance of EEG recordings with respect to cerebral perfusion.
increase in high-frequency PSD and a decrease in low-frequency PSD. Cerebral hemodynamic changes after anastomosis are complicated, and hemodynamic stability is difficult to maintain during combined revascularization.

The functional role of the overall change in high-frequency PSD remains unclear. In a recent review, the beta band was associated with response inhibition. Beta oscillatory responses were also found to be positively related to somatosensory and motor functions. In another study, beta band activity reflected arousal of the visual system during increased visual attention. For the gamma band, gamma rhythms are believed to represent the binding together of different neuronal populations into a network to carry out a certain cognitive or motor function. The earliest model of gamma oscillations was based on reciprocal connections between pools of excitatory pyramidal and inhibitory neurons. In another model of these neurons, axon conduction and synaptic delays lead to a phase shift between pyramidal and interneuron spikes, and these delays determine the frequency of the gamma rhythm [13].

5.2 DTABR

The change in DTABR was significantly correlated with NIHSS score improvement. This supports the use
Fig. 5. Correlations between the post-/pre-bypass PSD and DTABR ratios for the nonbypass area and MMSE score change. PSD, power spectral density; DTABR, (delta+theta)/(alpha+beta) ratio; MMSE, Mini-Mental State Examination.

of iECoG parameters (such as DTABR) in prognostication regarding MMD patients undergoing revascularization surgery, which is in line with previous findings. In 26 patients with subacute ischemic stroke in the middle cerebral artery territory, Z-values of absolute delta power (derived using a normative population database) displayed a higher prognostic value compared to the Canadian Neurological Scale regarding 3-month stroke outcomes measured by the modified Rankin Scale [25]. Finnigan et al. [14] obtained the acute delta change index (aDCI) from two recordings and compared it to serial diffusion-weighted magnetic resonance imaging (DWI) and perfusion-weighted magnetic resonance imaging (PWI) data from 11 patients within 16 h after the onset of confirmed stroke symptoms. The correlation between aDCI and the 30-day NIHSS score was higher than that between aDCI and initial DWI lesion volumes [14]. Furthermore, in 13 patients with subacute ischemic stroke, DAR and relative alpha power were sig-
Fig. 6. Differences in the DTABR ratio and PSD of each frequency band in the bypass area between the complication and noncomplication groups. Significant differences were found in the DTABR ratio and PSD of the theta band. PSD, power spectral density; DTABR, ((delta+theta)/(alpha+beta)) ratio.
significantly correlated with the 30-day NIHSS score. Finnigan et al. [14] also found the DAR to be the most effective QEEG measure for prognostication regarding the evolution of cerebral ischemia. In comparison to the DAR, the DTABR evaluates theta and beta activity as well, both of which may be altered by strokes [26–28].

5.3 Postoperative complications

In our study, there was a significant difference in the incidence of postoperative transient neurological dysfunction between the precision bypass group and the traditional group, while no significant difference was found in the incidence of postoperative complications such as cerebral infarction and epilepsy. The phenomenon of hyperperfusion syndrome is one of the causes of transient neurologi-
cral dysfunction after direct bypass in MMD. In the precision bypass group, a relatively low perfusion area was selected for STA-MCA bypass surgery through iECoG monitoring, which may avoid local blood flow overperfusion and thus reduce the occurrence of postoperative TNEs. In the course of iECoG monitoring, we found that some patients had sporadic epileptiform discharge, which may be related to the occurrence of postoperative epilepsy. Our finding was expected because accumulating data suggest that high-frequency oscillations are biomarkers for the epileptogenic zone in nontumoral epilepsies [29]. However, under the premise that the clinical significance of this phenomenon was not clear, we did not make special adjustments to postoperative antiepileptic therapy. We believe that if the occurrence of postoperative epilepsy can be predicted by iECoG monitoring and if drug intervention can be carried out in advance, then the incidence of postoperative epilepsy can also be effectively controlled.

The results indicated that the post-/pre-bypass DTABR ratio was significantly higher among the patients with postoperative complications than among those without complications. The increase in postoperative DTABR indicates an increase in postoperative cortical ischemia. Although combined bypass surgery clearly has an immediate positive effect on cerebral hemodynamics, postoperative hemodynamic instability still needs more study. Using QEEG, we can not only predict the occurrence of postoperative complications quantitatively but also provide a reliable and effective tool for future research.

As a pioneer study to explore the correlation between iECoG and bypass surgery, our study had several limitations. The first was the small sample size of 26 patients, which led to insufficient statistical power. We believe that increasing the sample size in a future study will increase the statistical significance of the existing indicators and allow more indicators to be discovered. Another possible limitation of our study was the relative stationarity of the iECoG recordings. Intraoperative influences, including the use of a bipolar electric coagulation knife, can be removed artificially during data processing but cannot be completely avoided. The intrinsic PSD characteristics of different brain regions may affect the intraoperative judgment of cortical hypoperfusion regions, which may partly explain why the overall perioperative complication rate in the precision bypass group was not significantly lower than that in the conventional group. Due to the intrinsic properties of the evaluated iECoG parameters, there are some differences in cortical electrical activities or frequency power between awake patients and anesthetized MMD patients. What’s more, there is few literatures specifically investigating the relationship between perfusion status and frequency bands in the setting of anesthesia, which need further researches. Finally, we were unable to compare the ischemic stroke-related EEG effects between affected and unaffected hemispheres and to assess their correlations with functional outcomes.

6. Conclusions
Our study confirmed that cortical electrophysiological monitoring could sensitively reflect changes in cortical blood flow during bypass surgery. QEEG parameters have good predictive value for the improvement of postoperative neurological function, neuropsychological performance and the occurrence of complications in patients with MMD. Cortical electrophysiological monitoring could be used as a potential reference for vascular selection in patients undergoing bypass surgery.

Abbreviations
MMD, moyamoya disease; iECoG, intraoperative electrocorticography; PSD, power spectral density; DTABR, (delta+theta)/(alpha+beta) ratio.

Author contributions
XZ and JS performed all data acquisition and interpretation and drafted the manuscript. JY assisted with data interpretation and revised the manuscript. YJL, SY, HY and CG assisted with data collection. WN, YL, RF and YG guided article revision. All authors contributed to the article and approved the submitted version.

Ethics approval and consent to participate
All procedures in this study were conducted in accordance with the Institutional Review Board in Huashan Hospital, Fudan University, China (approval No. 2014-278). Written informed consent was obtained from the patients for their anonymized information to be published in this article.

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Conflict of interest
The authors declare no conflict of interest.

12. References
[1] Scott RM, Smith ER. Moyamoya disease and moyamoya syndrome. The New England Journal of Medicine. 2009; 360: 1226–1237.
Zhao M, Deng X, Zhang D, Wang S, Zhang Y, Wang R, et al. Risk factors for and outcomes of postoperative complications in adult patients with moyamoya disease. Journal of Neurosurgery. 2019; 2: 476–485.

Yang T, Higashino Y, Kataoka H, Hamano E, Maruyama D, Ihara K, et al. Correlation between reduction in microvascular transit time after superficial temporal artery-middle cerebral artery bypass surgery for moyamoya disease and the development of postoperative hyperperfusion syndrome. Journal of Neurosurgery. 2019; 128: 1304–1310.

Zhang X, Ni W, Feng R, Li Y, Lei Y, Xia D, et al. Evaluation of Hemodynamic Change by Indocyanine Green-FLOW 800 Videoangiography Mapping: Prediction of Hyperperfusion Syndrome in Patients with Moyamoya Disease. Oxidative Medicine and Cellular Longevity. 2020; 2020: 8561609.

Accornore N, Capozza M, Pieroni L, Pro S, Davi L, Mecarelli O. EEG mean frequency changes in healthy subjects during prefrontal transcranial direct current stimulation. Journal of Neurophysiology. 2014; 112: 1367–1375.

Gollwitzer S, Müller TM, Hopfgartner R, Rampp S, Merkel J, Hagge M, et al. Quantitative EEG after Subarachnoid Hemorrhage Predicts Long-Term Functional Outcome. Journal of Clinical Neurophysiology. 2019; 36: 25–31.

Gollwitzer S, Groemer T, Rampp S, Hagge M, Olmes D, Huttner HB, et al. Early prediction of delayed cerebral ischemia in subarachnoid hemorrhage based on quantitative EEG: a prospective study in adults. Clinical Neurophysiology. 2015; 126: 1514–1523.

Geoæadin RG, Ghodadra R, Kimura T, Lei H, Sherman DL, Hanley DF, et al. A novel quantitative EEG injury measure of global cerebral ischemia. Clinical Neurophysiology. 2000; 111: 1779–1787.

Liu S, Quach MM, Curry DJ, Umnat M, Seto E, Ince NF. High-frequency oscillations detected in ECoG recordings correlate with cavaufusion malformation and seizure-free outcome in a child with focal epilepsy: a case report. Epilepsia Open. 2017; 2: 267–272.

Jacobs J, Wu JY, Perucca P, Zelnmann R, Mader M, Dubeau F, et al. Removing high-frequency oscillations: A prospective multicenter study on seizure outcome. Neurology. 2018; 91: e1040–e1052.

Finnigan S, van Putten MJAM. EEG in ischaemic stroke: Quantitative EEG can uniquely inform (sub)-acute prognoses and clinical management. Clinical Neurophysiology. 2013; 124: 10–19.

Finnigan S, Wong A, Read S. Defining abnormal slow EEG activity in acute ischaemic stroke: Delta/alpha ratio as an optimal QEEG index. Clinical Neurophysiology. 2016; 127: 1452–1459.

Noshiro S, Mikami T, Komatsu K, Kanno A, Enatsu R, Yazawa S, et al. Neuroromodulatory Role of Revascularization Surgery in Moyamoya Disease. World Neurosurgery. 2016; 91: 473–482.

Finnigan SP, Rose SE, Walsh M, Griffin M, Janke AL, McMahon KL, et al. Correlation of Quantitative EEG in Acute Ischemic Stroke with 30-Day NIHSS Score: comparison with diffusion and perfusion MRI. Stroke. 2004; 35: 899–903.

Rots ML, van Putten MJAM, Hoedemakers CWE, Horn J. Continuous EEG Monitoring for Early Detection of Delayed Cerebral Ischemia in Subarachnoid Hemorrhage: a Pilot Study. Neurocritical Care. 2016; 24: 207–216.

Sheikh N, Wong A, Read S, Coulthard A, Finnigan S. QEEG may uniquely inform and expedite decisions regarding intracranial clot retrieval in acute stroke. Clinical Neurophysiology 2013; 124: 1913–1914.

Sheorajpanday RVA, Nagels G, Weeren AJTM, van Putten MJAM, De Deyn PP. Quantitative EEG in ischemic stroke: Correlation with functional status after 6 months. Clinical Neurophysiology. 2011; 122: 874–883.

Stuart RM, Waziri A, Weintraub D, Schmidt MJ, Fernandez L, Helbok R, et al. Intracortical EEG for the detection of vasospasm in patients with poor-grade subarachnoid hemorrhage. Neurocritical Care. 2010; 13: 355–358.

Ni W, Jiang H, Xu B, Lei Y, Yang H, Su J, et al. Treatment of aneurysms in patients with moyamoya disease: a 10-year single-center experience. Journal of Neurosurgery. 2018; 128: 1813–1822.

Komura S, Mikami T, Sugino T, Suzuki Y, Komatsu K, Wanibuchi M, et al. Complementary Relation between Direct and Indirect Bypass in Progress of Collateral Circulation in Moyamoya Disease. World Neurosurgery. 2017; 104: 197–204.

Acker G, Fekonja L, Vajkoczy P. Surgical Management of Moyamoya Disease. World Neurosurgery. 2016; 91: 473–482.

Berger A, Pixa NH, Steinberg F, Doppelmayr M. Brain Oscillatory and Hemodynamic Activity in a Bimanual Coordination Task Following Transcranial Alternating Current Stimulation (tACS): A Combined EEG-mNIRS Study. Frontiers in Behavioral Neuroscience. 2018; 12: 67.

Leemburg S, Gao B, Cam E, Sarnthein J, Bassetti CL. Power spectrum slope is related to motor function after focal cerebral ischemia in the rat. Sleep. 2018; 41: zsy132.

Roberts JM, Bechara J, Middleton S, Johnstone SJ. Acute EEG Patterns Associated with Transient Ischemic Attack. Clinical EEG and Neuroscience. 2019; 50: 196–204.

Veenes MM, Monkman EJ, Poortvliet DC, De Weerd AW, Tans JT, John ER. The effect of reconstructive vascular surgery on clinical status, quantitative EEG and cerebral blood flow in patients with cerebral ischaemia. A three month follow-up study in operated and unoperated stroke patients. Electroencephalography and Clinical Neurophysiology. 1986; 64: 383–393.

McVoy M, Lytle S, Fulchiero E, Aebi ME, Adelaye O, Sajatovic M. A systematic review of quantitative EEG as a possible biomarker in child psychiatric disorders. Psychiatry Research. 2019; 279: 331–344.

Kramer MA, Ostrowski LM, Song DY, Thorn EL, Stoyell SM, Parnes M, et al. Sculp recorded spike ripples predict seizure risk in childhood epilepsy better than spikes. Brain. 2019; 142: 1296–1309.

Vriens EM, Wienieke GH, Van Huffelen AC, Visser GH, Eikelboom BC. Increase in alpha rhythm frequency after carotid endarterectomy. Clinical Neurophysiology. 2000; 111: 1503–1513.

Wickerling E, Gaspard N, Zafar S, Moura VI, Bisswal S, Beechek S, et al. Automation of Classical QEEG Trending Methods for Early Detection of Delayed Cerebral Ischemia: More Work to Do. Journal of Clinical Neurophysiology. 2016; 33: 227–234.