Translucency of monolithic and core zirconia after hydrothermal aging

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ABSTRACT

Objective: To evaluate the hydrothermal aging effect on the translucency of partially stabilized tetragonal zirconia with yttria (Y-TZP) used as monolithic or fully milled zirconia and of core type.

Methods: Twenty disc-shaped specimens (1 and 10 mm) for each type of monolithic and core Y-TZP materials were milled and sintered according to the manufacturer’s instruction. The final specimens were divided into two groups according to the type of Y-TZP used. Translucency parameter (TP) was measured over white and black backgrounds with the diffuse reflectance method; X-ray diffraction (XRD) and scanning electron microscope (SEM) were used to analyze the microstructure of both Y-TZP types before and after aging. Data for TP values was statistically analyzed using Student’s t-test.

Results: Monolithic Y-TZP showed the highest TP mean value (16.4 ± 0.316) before aging while core Y-TZP showed the lowest TP mean value (7.05 ± 0.261) after aging. There was a significant difference between the two Y-TZP types before and after hydrothermal aging. XRD analysis showed increases in monoclinic content in both Y-TZP surfaces after aging.

Conclusion: Monolithic Y-TZP has a higher chance to low-temperature degradation than core type, which may significantly affect the esthetic appearance and translucency hence durability of translucent Y-TZP.

Introduction

Dental all-ceramic restorations have been used as an alternative to metal ceramic restorations due to their excellent esthetics, chemical stability and biocompatibility.[1–6] Zirconia (ZrO₂) has rapidly achieved a leading position among the polycrystalline ceramic dental restorative materials. It is used as a framework for crowns or fixed partial dentures as well as oral implants.[7,8] The partially stabilized tetragonal zirconia with yttria (Y-TZP) was introduced to dentistry as a core material for all-ceramic restorations and has been made available through the computer-aided design/computer-aided milling (CAD/CAM) technique. Even though reports about ZrO₂ as core material indicate that these frameworks have excellent fracture resistance, the problem of chipping and fracture of ceramic veneer has been reported as a common technical problem.[9,10] This is in addition to the opaqueness of ZrO₂ core, which should be masked with a translucent layer of veneer ceramic to achieve the natural appearance of tooth structure. The color of this opaque core significantly influences esthetic of all-ceramic restoration.[11–13] Recently, it has become possible to fabricate all-ceramic restorations with high resistant to fracture, even when they are used in the posterior region, by using ZrO₂-based materials due to its good mechanical properties and tooth-like appearance.[14,15] This ZrO₂ has many advantages over the porcelain-veneered ZrO₂ copings in that no liability of veneering fracture or chipping as it is already absent, beside the high strength that is reported to be comparable to previous all-ceramic crowns as well as a patent shading system that enables high esthetic matching. All these advantages allow less axial walls and occlusal reduction in tooth structure to be done. The absence of added porcelain veneer procedures, which may be responsible for the induced stresses in ZrO₂ core/veneer interface in layered restorations, may be also considered as an additional advantage.[16] However, the fact of exposing ZrO₂ surface to the oral environment in monolithic restorations makes it even more liable to the commonly named low-temperature degradation (LTD) than core type covered with porcelain veneer. It happens due to progressive and spontaneous transformation of the metastable tetragonal (t) phase into the monoclinic (m) phase (t-m transformation) when this transformation is not triggered by local stresses produced by advancing crack.[16–18] The LTD of monolithic ZrO₂...
may be considered as an important factor affecting the durability of fine-grained metastable microstructure and stability of \( t \) grains during the lifetime of TZP components, which is the key-point to attain the expected performance of Y-TZP.[19–21] The aim of the present study was to evaluate the effect of hydrothermal aging on the translucency of monolithic \( \text{ZrO}_2 \) used for full coverage dental restorations in comparison with core \( \text{ZrO}_2 \) type.

**Materials and methods**

Forty disc-shaped specimens (10 mm in diameter and 1 mm in thickness) from both monolithic and core Y-TZP types were prepared. They were divided into two groups according to the type of \( \text{ZrO}_2 \) used (i.e. \( n = 20 \)). The two groups were further subdivided according to whether being subjected to hydrothermal aging or not. Hydrothermal aging was performed using an autoclave (CISA S.p.A., Pomezia, Rome, Italy) at 134°C and under pressure two bars for 15 h.[22]

**Preparation of monolithic specimens**

They were fabricated using Y-TZP pre-sintered cake block (Zirkonzahn Prettau, Zirkonzahn GmbH, Bruneck, Italy). A resin pattern (10 \( \times \) 1 mm) was prepared from the self-cured acrylic resin (Pattern Resin LS, GC America Inc., Alsip IL). The thickness of 1 mm was previously recommended for monolithic \( \text{ZrO}_2 \).[23] The resin pattern was fixed on one side of the milling table of Zirkonzahn milling system (Zirkograph 025 ECO, Zirkonzahn GmbH) while Prettau Y-TZP block was fixed on the other side of the table. The milled specimen was 20–25% larger than the resin pattern to compensate for the sintering shrinkage. Specimens were prepared by copy-milling, carefully removed from the milled blank and lightly finished to remove any sharp margins using silicon carbide papers (grits 400, 600 \( \mu \)m) under water to remove any sharp edges or points and minimize the finishing and polishing after sintering. Shade \( A_2 \) stain was applied to all the specimens. Sintering was done using \( \text{ZrO}_2 \) oven (Zirkonofen 600, Zirkonzahn). The oven temperature was raised to 1600°C within 4 h, kept at this temperature for 2 h and then gradually decreased within another 2 h, according to manufacturer’s instructions. After complete cooling to room temperature, the discs were finally polished from both sides using a polishing paste (Meta Di, grain size (GS) 1 \( \mu \)m, Düsseldorf, Germany) with minimal pressure and under water to final monolithic specimens.

**Preparation of core \( \text{ZrO}_2 \)**

Core specimens were fabricated using Y-TZP (Lava frame, 3M-ESPE, St. Paul, MN) using resin pattern (10 \( \times \) 1 mm) and copy-milling machine by the same technique for the monolithic specimen. They received shade \( A_2 \) and sintered using Lava oven (Lava furnace 200, 3M ESPE). Oven temperature was 1500°C for 8 h, according to manufacturer’s instructions. Specimens were finally polished. Materials used in the present study are summarized in Table 1.

**Crystal microstructure**

X-ray diffractometer (X’Pert Pro, PANalytical B.V. company, Costa da Caparica, Portugal) was used to analyze the microstructure of both \( \text{ZrO}_2 \) types before and after hydrothermal aging. Data were collected from the diffraction angle (2\( \theta \)) ranges between 25 and 79° and in step size (2\( \theta \)) 0.02° with 1 s dwell time. Standard patterns or models for each of the three \( \text{ZrO}_2 \) phases (tetragonal, cubic and monoclinic) were used for comparison and refinement of the obtained phase structure. The volume of monoclinic phase (\( V_m \)) was quantified according to Garvie and Nicholson approach.[24] The \( V_m \) was determined by measuring the height of two nearest \( m \) peaks in relation to the main T/C main peak detected at nearly 30.1° 2\( \theta \) according to the following equation:

\[
V_m = \frac{\text{Height of } M_1 + \text{Height of } M_2}{\text{Height of } M_1 + \text{Height of } M_2 + \text{Height of T/C}} \times 100
\]

where, \( M_1 \) is monoclinic peak at 28.2° 2\( \theta \), \( M_2 \) is monoclinic peak at 31.9° 2\( \theta \) and T/C is a tetragonal/cubic (T/C) peak at 30.1° 2\( \theta \).

Intensity counts were used as indication for degree of crystallinity and the average crystal size (L), before and after aging, was calculated from the “Scherrer formula” as follows:[25]

\[
L = \frac{K\lambda}{\beta \cos \theta}
\]

where \( \lambda \) is the X-ray wavelength in nanometer (nm), \( \beta \) is the peak width of the diffraction peak profile at half maximum height resulting from small crystallite size and \( K \) is a constant related to crystallite shape (0.9).

**Translucency test**

The translucency parameter (TP) of two \( \text{ZrO}_2 \) types was detected using the spectrophotometer (UV Shimadzu 3101 PC, UV-VIS-NIR Scanning Spectrophotometer, Tokyo, Japan) before and after hydrothermal aging through diffuse reflectance method. The TP was detected by calculating the color difference for each specimen.
when it was placed over a black background or reference (0 lightness) and then over a white background or reference (100 lightness, barium sulfate pressed powder). Each specimen was subjected to the light source, which applies to the CIE (Commission Internationale de l’Eclairage) standard illumination requirements. The CIE-Lab color co-ordinates ($L^*, a^*, b^*$) for each specimen were then calculated in several steps via a special software (MATLAB, MathWorks, Inc., Michigan, United States) in both conditions of black and white backgrounds. The TP was calculated through the following equation:

$$TP = \left( L_B^* - L_W^* \right)^2 + \left( a_B^* - a_W^* \right)^2 + \left( b_B^* - b_W^* \right)^2$$

where $L_B^*$ is the value (lightness) over a black reference while $L_W^*$ is the value over white reference, $a_B^*$ and $a_W^*$ are red-green coordinates values over black and white references, respectively, $b_B^*$ and $b_W^*$ are blue-yellow coordinates values over black and white references, respectively.[26,27]

### Scanning electron microscope (SEM) analysis

It was done using gold-coated ZrO$_2$ surfaces and scanned using SEM (JEOL, JSM-5300-Japan-Scanning Electron Microscope, Tokyo, Japan) to study the shape and compaction of grains for ZrO$_2$ types.

### Results

#### Crystal microstructure

Dominant T/C peak for core Y-TZP appeared at an approximate position of 30.5°2θ (111 hkl) before aging while the T/C peak appeared at 50.5°2θ (112 hkl) was in a higher position relative to that peak at 30.1°2θ with no apparent monoclinic peaks. Dominant monoclinic peaks appeared at 28.7 and 28.5°2θ (−111 hkl) of the aged pattern in both Y-TZP types. Core Y-TZP showed higher crystal intensity counts (up to 800) (Figure 1 a and b) while monolithic Y-TZP showed lower crystal intensity counts (up to 200) (Figure 2 a and b) in X-ray patterns before and after aging. Aged monolithic specimens showed $V_m$ of 25% while aged core Y-TZP specimens showed $V_m$ values of 18% after accelerated hydrothermal aging (Table 2). Regarding average crystal size, monolithic Y-TZP showed larger average crystal size than core type before and after aging. After aging, the crystal size was decreased for both monolithic and core Y-TZP types (30.243 and 22.612 nm, respectively) (Table 3).
Translucency test

Monolithic Y-TZP showed the highest mean values (16.4 ± 0.316 and 13.35 ± 0.158), before and after aging, respectively. However, core Y-TZP showed the lowest mean translucency values (9.38 ± 0.395 and 7.05 ± 0.261), before and after aging, respectively. Comparing the mean translucency values for both types of Y-TZP before and after aging was done using Student’s t-test. It showed that there was a significant difference between core (p = 0.0001) and monolithic Y-TZP (p = 0.0001) before and after aging. There was a statistical significant difference within both core and monolithic groups (p = 0.0001 and 0.0001) before and after hydrothermal aging, respectively (Table 4).

Table 2. Volumetric monoclinic phase content of aged Y-TZP (V_m).

| Y-TZP Type | V_m (%) |
|------------|---------|
| Monolithic | 25.0    |
| Core       | 18.0    |

V_m, monoclinic volume after aging.

Table 3. Average grain particle size for both Y-TZP types before and after aging.

| Y-TZP Type | Average crystal size (nm) |
|------------|---------------------------|
| Monolithic | Before aging: 49.682       |
|            | After aging: 30.243       |
| Core       | Before aging: 34.915       |
|            | After aging: 22.612       |

Table 4. Student’s t-test of translucency for both materials before and after aging.

| Material | Translucency | Before | After | T value | p value |
|----------|--------------|--------|-------|---------|---------|
|          | Mean | SD  | Mean | SD  |        |        |
| Monolithic | 16.4 | 0.316 | 13.35 | 0.158 | 19.3 | 0.0001* |
| Core      | 9.38 | 0.395 | 7.05  | 0.261 | 8.53 | 0.0001* |
| T value   | 31.3 | 45.9  |       |       |       |         |
| p value   | 0.0001* | 0.0001* |       |       |       |         |

* significant difference at P value ≤ 0.05.

**SEM analysis**

It showed that monolithic Y-TZP showed less dense grain structure (×5000) than did core type appeared at the same magnification power (Figures 3 and 4, respectively).

**Discussion**

Recently, the introduction of monolithic Y-TZP with improved translucency in an attempt to overcome the veneer chipping and opacity problems was accomplished successfully.16 However, ZrO_2 LTD issue and its effect on a monolithic type, in comparison with core ZrO_2, needs more comprehensive study.

**Crystal microstructure**

ZrO_2 LTD and any deterioration in the properties are accompanied by microstructural changes and an increase in monoclinic content. Accelerated hydrothermal aging, simulating the oral environment, was done using autoclave at 134°C and pressure two bars for 15 h, which is...
It was reported that placing 3-mol Y-TZP for 1 h in an autoclave at 134°C and pressure two bars is equivalent to 3–4 years at 37°C.[28,29] The X-ray diffraction (XRD) patterns of both types of Y-TZP (monolithic and core) before aging revealed the presence of T/C phases. The dominant T/C appeared at nearly 30.6°2θ (111 hkl) in both types of ZrO₂. This is in agreement with the phase diagram of ZrO₂ in which ZrO₂ having 3-mol Y₂O₃ in the composition should present two phases (T/C) microstructure when sintered at 1400–1500°C.[28] Both Y-TZP types revealed monoclinic peaks appearance at 28.5° 2θ (~111 hkl) after aging, which agrees with the previous findings of an increase in monoclinic content after hydrothermal aging.[29–41] Core Y-TZP showed higher resistance to LTD than monolithic type. This may be attributed to the finding of having smaller average crystal sizes than monolithic Y-TZP. It was reported previously that larger grains are less resistant to transformation but more favorable to mechanical properties.[36] Reducing the GS of metastable t-ZrO₂ ceramics has a beneficial effect as it reduces the thermodynamic driving force for transformation. Although, there was, up till now, no clinical evidence of

Figure 3. SEM images of monolithic Y-TZP before aging showing the less dense structure before aging (magnification 5000).

Figure 4. SEM images of core Y-TZP before aging showing the more dense structure before aging (magnification 5000).
LTD in dental ZrO\textsubscript{2} but the combination of large grain sizes and oral humid environment can precipitate such autocatalytic degradation.[37]

**Translucency**

Core Y-TZP is known to be of low translucency, even if it has a high translucent porcelain veneer due to its low refractive index, low absorption coefficient and high opacity in visible and infrared regions of the spectrum.[27] The significant difference in TP values between the two Y-TZP types used in the present study may be explained through the XRD microstructure analysis results. It was found that core Y-TZP was characterized by smaller average GS of the dispersed particles and showed higher intensity counts and lower TP values than monolithic type, which showed higher values for GS and intensity counts. This is in accordance with a previous study where ceramics with a high degree of crystallinity showed lower translucency values. The smaller GS with a higher degree of crystallinity may lead more scattering of the incident light and hence higher opacity with lower translucency and vice versa.[27,38]

There was a significant decrease in TP values in both types of Y-TZP after 15 h of hydrothermal aging. This may be attributed to the increase in monoclinic content $V_m$ after aging in both materials. It is in agreement with previous studies [22,39] where the appearance of monoclinic phase on the surface is accompanied by formation of microcracking as well as the monoclinic phase itself may act as a flaw or defect in ZrO\textsubscript{2} microstructure. These microcracking may act as porosity or defects enhancing scattering of incident light beam thus reducing translucency. The presence of voids or porosities as well as material’s thickness, crystallinity and grain size may all act as various factors affecting light scattering and consequently lead to impairment of translucency.[38] The co-existence of different phases (monoclinic and T/C) after hydrothermal aging may have been contributed to increase in refractive indices of an incident light beam by various phases and hence decreasing the translucency values.[40,41] Gain size and hence grain boundaries also have a great effect on translucency. The larger grain size reported to have higher translucency like what was found in monolithic ZrO\textsubscript{2} in the present study due to larger grain boundaries.[36]

**Conclusion**

Within the limitations of the present study, the recently introduced translucent Y-TZP used as monolithic crowns and bridges showed significant higher translucency than core type when it is subjected to hydrothermal aging for 15 h. On the other hand, it has higher susceptibility to LTD that may negatively affect its durability that needs further investigations especially on its mechanical properties.

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**Declaration of interest**

The authors report no conflicts of interest. The authors alone are responsible for the content and writing of this article.

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