A Review of Deep Learning Approaches to EEG-Based Classification of Cybersickness in Virtual Reality

Caglar Yildirim
Khoury College of Computer Sciences
Northeastern University
Boston, MA
c.yildirim@northeastern.edu

Abstract—Cybersickness is an unpleasant side effect of exposure to a virtual reality (VR) experience and refers to such physiological repercussions as nausea and dizziness triggered in response to VR exposure. Given the debilitating effect of cybersickness on the user experience in VR, academic interest in the automatic detection of cybersickness from physiological measurements has crested in recent years. Electroencephalography (EEG) has been extensively used to capture changes in electrical activity in the brain and to automatically classify cybersickness from brainwaves using a variety of machine learning algorithms. Recent advances in deep learning (DL) algorithms and increasing availability of computational resources for DL have paved the way for a new area of research into the application of DL frameworks to EEG-based detection of cybersickness. Accordingly, this review involved a systematic review of the peer-reviewed papers concerned with the application of DL frameworks to the classification of cybersickness from EEG signals. The relevant literature was identified through exhaustive database searches, and the papers were scrutinized with respect to experimental protocols for data collection, data preprocessing, and DL architectures. The review revealed a limited number of studies in this nascent area of research and showed that the DL frameworks reported in these studies (i.e., DNN, CNN, and RNN) could classify cybersickness with an average accuracy rate of 93%. This review provides a summary of the trends and issues in the application of DL frameworks to the EEG-based detection of cybersickness, with some guidelines for future research.

Keywords—cybersickness, deep learning, EEG, EEG-based, brainwaves, neural networks

I. INTRODUCTION

Coeval with the virtual reality (VR) technology itself, cybersickness, or simulator sickness, denotes the affereffects of exposure to VR, commonly characterized by such physiological symptoms as nausea, dizziness, sweating, and lightheadedness [1 - 3]. While different accounts of the causes of cybersickness are available in the literature [4], sensory mismatch theory is commonly regarded as the most plausible explanation for the occurrence of cybersickness [5]. According to the sensory mismatch theory [6, 7], cybersickness arises from a mismatch between visual and vestibular systems while users are exposed to a VR experience. More specifically, the vestibular feedback provided to the user by the vestibular system falls short of accounting for the visual feedback provided by the virtual environment (VE) to produce a virtual locomotion effect. This happens because the vestibular system works on the basis of the vestibular cues provided by the physical environment (not the VE) in response to the position, movement, and orientation of the user in the physical environment. When these vestibular cues are not in accordance with the visual stimuli associated with the position, movement, and orientation of the user in the VE, this leads to a visual-vestibular mismatch, which in turn causes cybersickness [1, 4, 5].

Given the long-standing prevalence of cybersickness in VR, even when using state-of-the-art VR head-mounted displays (HMDs) [3], the measurement of cybersickness has been of particular interest to researchers. The majority of the studies in the literature have exclusively utilized self-reported measures of cybersickness to determine whether users experience cybersickness during a VR experience and to quantify its severity [1, 4]. For instance, one commonly-used self-reported instrument is the Kennedy Simulator Sickness Questionnaire [8], which is now the standard self-reported measure of cybersickness [5]. While these self-reported measures have been shown to yield valid and reliable measurements of cybersickness, they are subjective in nature. Therefore, there has lately been an increasing interest in objectively determining the occurrence of cybersickness based on physiological changes observed during VR exposure [9].

Previous studies have attempted to objectively detect cybersickness from heart rate and heart rate variability [10-12], skin conductance levels [11, 12], and respiration rate [11, 12]. Because of the cognitive and neurovegetative changes associated with cybersickness, brainwaves obtained through electroencephalogram (EEG) have also been used to objectively detect cybersickness [13-19]. Given that such an attempt requires automatic detection of cybersickness on the basis of patterns observed in EEG signals, traditional machine learning algorithms (e.g., Support Vector Machines, Naïve Bayes, and k-Nearest Neighbors) have been extensively applied to the analysis of EEG data for automatic cybersickness detection [20-25]. Moreover, recent advances in deep learning (DL) algorithms, which are aimed at learning representations from data in successive layers of processing in neural networks, and increasing availability of computational resources for DL have paved the way for the application of DL frameworks to EEG-based detection of cybersickness [26-29].
This paper provides a systematic review of the peer-reviewed literature on the application of DL frameworks to the analysis of EEG-data to detect cybersickness during VR exposure. The goals of this review were (a) to compile the relevant studies in this burgeoning area of research, (b) to identify the trends and issues in the use of DL frameworks when classifying EEG-data to detect cybersickness, and (c) to provide methodological guidelines for the design of EEG-based VR experiments for cybersickness detection, preprocessing of data, and selection of DL architectures and hyperparameters.

II. METHOD

A. Literature Search

To identify the relevant papers in the literature, repeated searches were conducted on three commonly used databases, namely Web of Science, PubMed, and Google Scholar. Because the application of deep learning to the classification of cybersickness levels using EEG data is rather specific, the original database search was performed to include a wider array of papers, using the following keyword combinations: ((cybersickness OR motion sickness OR simulator sickness) AND (EEG OR electroencephalogram OR electroencephalography OR brainwaves OR brain signals OR physiological))

This original search was performed to search through all fields for a given paper and resulted in a total of 408, which was further refined to yield 132 results after filtering and eliminating duplicates. Upon a closer look at the results through their title and abstract, the list of papers was reduced to 33 results.

B. Eligibility Criteria

In order for a paper to be included in this review, it needed to meet certain eligibility criteria. To begin with, the paper should have attempted to predict cybersickness as the target variable. The paper should also have investigated cybersickness in VR interactions using an HMD. Given the proliferation of modern HMDs, cybersickness is a more prevalent issue for HMDs. Furthermore, EEG patterns observed when participants wear an HMD are expected to be different from those observed when users interact with a CAVE-like immersive environment. Finally, the paper should have collected EEG data and should have used at least one DL architecture.

C. Screening

The refined list of 33 papers was screened according to the eligibility criteria described in the previous section. Some 13 of these papers were excluded from this review because no deep learning technique was used in the paper. Similarly, nine papers were excluded for not having collected and used EEG data to predict cybersickness and six papers for not having used an HMD. Lastly, one paper was a review paper reporting no empirical data. This screening resulted in a final list of four papers that meet the eligibility criteria [26-29]. Therefore, the current review focused on these four papers.

III. RESULTS

The final list of four papers [26-29] included in this review were closely scrutinized and encoded to capture a variety of attributes in relation to experimental procedures, data preprocessing steps, and DL architecture choices. Table 1 provides a detailed summary of these papers.

A. Experimental Design

Experimental design plays a pivotal role when integrating EEG measurements into human-computer interaction experiments in VR. The overall experimental procedure followed by a study directly influences whether DL techniques can be applied to the analysis of the data collected from the experiment. Therefore, in what follows a detailed description of the various experimental design choices made by the previous studies is provided as a practical guide for future studies into this nascent area of research.

1) EEG Devices

Some of the early studies into EEG-based classification of cybersickness levels have used research grade EEG devices [15]. While these EEG devices provide reliable measurements of electrical activity in the brain, they present unique challenges when combined with head-mounted VR headsets in terms of placing both the EEG device and VR headset on users’ head at the same time. Therefore, there has been an increasing interest in the use of non-invasive, wireless EEG devices to measure cybersickness while participants wear an HMD [13]. This trend was also observed in the studies included in this review. In fact, with the exception of [26], the remaining three studies used a non-invasive, wireless EEG device to capture brain activity (Emotiv Epoc+ or Neurosky MindWave).

Emotiv Epoc+ is a 14-channel wireless EEG device and is perhaps one of the most commonly used mobile EEG solutions available. While the availability of 14 channels is an advantage, the physical shape of the device and how it needs to be fitted on users’ head may represent a challenge in future studies. The reason is that if not fitted properly, Emotiv Epoc+ readings will be unreliable. NeuroSky MindWave, on the other hand, is a single-channel EEG device placed on the forehead and collects data from the FP1 position. Admittedly, collecting brain activity data through a single channel has apparent downsides when compared to Emotiv Epoc+. That said, the placement of NeuroSky MindWave headset on users’ head is substantially easier and works better with a VR HMD than does Emotiv Epoc+. Considering the fact that these two wireless EEG devices have not been designed with VR integration in mind, there will be some tradeoffs when using these devices in future VR experiments. One potential alternative to these devices is LooxidLink (https://looxidlabs.com/looxidlink/), which is a wireless, 6-channel EEG device designed to be easily attached to modern VR HMDs, such as Oculus Rift and HTC VIVE.
TABLE I. SUMMARY OF REVIEW STUDIES

| Study | EEG Device | VR Content | Data | Classification Type | Preprocessing | Algorithm | Hyperparameters | Accuracy |
|-------|------------|------------|------|---------------------|---------------|-----------|-----------------|----------|
| [26]  | 8-channel  | 44 VR      | 30,663,600 | Multiclass (Likert scale rating) | Fourier Transform (FFT) | CNN | # Layers: 3 Activation: Leaky ReLU Optimizer: Adam Pooling: Max Batch normalization | 87.13%   |
|       | 250 Hz &   | videos (16s each) | | | | | | |
|       | 16 bits    |            | | | | | | |
| [27]  | 14-channel | 6 360-degree | 2,722,269 | Binary | Normalization Standardization | DNN | # Convnet Layers: 3 with (5,1) filter Max Pooling: 1 with (2,1) filter FC Layer: 1 with 100 nodes Activation: ReLU Output Activation: Sigmoid Dropout = 0.5 Early stopping | 98.82%   |
|       | Emotiv     | videos (1-5 min each) | | | | | | |
|       | Epoc+      |            | | | | | | |
| [28]  | 14-channel | 4 360-degree | 550,000 | Binary | Normalization Standardization | DNN | # Layers: 3 (128, 256, 128) Activation: ReLU Output Activation: Sigmoid Input shape: 84 Output shape: 32 Epochs = 1000 Dropout = 0.5 Early stopping | 99.12%   |
|       | Emotiv     | videos (2-3 min each) | | | | | | |
|       | Epoc+      |            | | | | | | |
| [29]  | NeuroSky   | 3 360-degree | 78,000 | Binary | FFT Power Spectral Density | RNN - LSTM | # Layers: 7 (32, 32, 32, 16, 16, 8, 8) Activation: ReLU Output Activation: Sigmoid Batch size: 100 Epochs: 125 L1 and L2 regularization Optimizer: RMSProp Time steps: 3 (1, 5, 10 min) Dropout = 0.5 Early stopping | 83.94%   |
|       | Mindwave   | videos (10 min in total) | | | | | | |

1) VR Headset

When studying cybersickness in VR, the VR headset used to view and interact with the VE is a key consideration. Based on the small number of studies included in the review, it can be said that various types of VR headsets have been used in prior research, including HTC VIVE, FOVE VR, and smartphone-based VR cardboard. Considering the recent release of untethered, light-weight VR headsets, such as Oculus Quest, we foresee that future research will witness the use of different VR headsets.

2) VR Environments

In cybersickness prediction studies, the goal is to ensure that some portion of the participants will experience a bearable amount of cybersickness, in order to differentiate between cybersickness and no-cybersickness classes.

To this end, previous studies have predominantly used 360-degree videos, which participants watched in VR. [26] used 44 short videos depicting an assortment of urban and astrospace scenes, all of which authors noted included visual motion. Similarly, the videos used by [27], [28] and [29] also included visual motion. In line with prior cybersickness research, roller coaster scenes were a popular choice in these previous studies [2-4]. The heavy use of VR content inducing visual motion during the VR experience is compatible with the prior work on the effect of visually-induced motion on cybersickness [13]. Therefore, future studies could utilize the same strategy as well.

One problem with these previous studies, however, is that users were passively exposed to these VR experiences with no explicit interaction between the user and VE. Based on the current evidence from these studies, it is unclear whether we would be able to predict cybersickness levels from EEG data using DL approaches when users are more actively engaged in the VE, as in the case of playing a VR game for instance. Thus, future studies should seek to incorporate different VR experiences with which users can interact to some extent. It should be noted, however, that frequent head and body movements could potentially add more noise to EEG data, which should be taken into account when preprocessing the data for analysis.
3) Cybersickness measures

In order to build a cybersickness detection framework, previous studies had users provide labels for the EEG data in the form of self-reported cybersickness levels. For this purpose, these studies used slightly different measures. To begin with, [26] used a multiclass classification approach and asked users to rate their cybersickness levels on a 5-point Likert scale (from 5-Extreme sickness to 1-Comfortable). The other three studies used a binary classification approach. [27] and [28] asked users to indicate whether they experienced cybersickness during VR exposure, which was dichotomously coded. [29], on the other hand, had users complete the SSQ. The authors then assigned a class label of “sickness” vs. “normal” based on users’ score on the SSQ. If the SSQ score was greater than 60, the class label was “sickness”, and it was “normal” otherwise.

Considering the problems associated with dividing users into cybersickness vs. no cybersickness classes based on an arbitrary cutoff score on a questionnaire, it might be a better idea to present to users a brief description of cybersickness and its symptoms at the end of the VR experience and to directly ask them to indicate whether or not they experienced cybersickness during their VR exposure. Based on the answer to this binary question, a follow-up question may be displayed, asking users to rate the severity of their cybersickness. Currently, there is a lack of comparative studies into the best approach to encoding the class variable, which is why future studies could build and test different models using these different approaches. Some open questions regarding the labeling of data are as follows: Does a binary classification task lead to better performance results, compared to a multiclass classification task? Is it better to use a dichotomous question or a standard questionnaire, such as SSQ?

4) Experimental procedures

All four studies have used similar procedures during data acquisition. In general, experimenters placed the EEG device and VR HMD on users’ head, and brain activity was captured during the VR experience. Users then provided self-reported ratings of their cybersickness levels. In the case of multiple VR experiences, users took short breaks to eliminate carry-over effects. One trend among the studies was that users were exposed to multiple VR experiences and provided self-reported assessments of their cybersickness levels for each. This way previous studies have been able to collect larger amounts of data than would be obtained using a single VR experience. For future studies, it would be prudent to devise multiple shorter VR experiences than a standalone long experience, especially when the number of users available for the experiment is limited. Regardless of the chunking of the content, all previous studies [26-29] exposed their participants to VR for a total of 10-15 minutes, which future studies could consider.

B. Data preprocessing

Given the sensitivity of EEG data to noise, raw electrical activity signals obtained through an EEG device are typically preprocessed before they are fed into a DL architecture. For studies in which the EEG device used to collect the data did not automatically extract power bands [26, 29], researchers applied Fast Fourier Transform (FFT) to raw EEG data to extract power bands (i.e., alpha, beta, gamma, delta, and theta). Once the power signals were available, the dataset was fed into the architecture without further preprocessing, except for normalization and standardization. [27] and [28] did in fact compare the effect of normalizing and standardizing feature vectors and found that standardized features led to a higher accuracy level than normalized features. One exception to this was [29], in which the authors also applied Power Spectral Density after FFT. As for the input formulation of the preprocessed EEG data into DL models, previous studies have exclusively relied on signal values for the different types of brainwaves, which were fed into the models [26-29].

C. DL Architectures

1) Architecture Design

The design of DL architectures for a given dataset is experimental in nature. This, coupled with the relatively recent application of DL approaches to VR research, translates into a burgeoning area of research at the intersection of machine learning and VR, which is challenging at the same time, as there are no established guidelines to aid researchers in their selection of various architecture designs.

The four studies included in this review have used deep neural networks (DNN), convolutional neural networks (CNN), and recurrent neural networks (RNN). DNNs are basic neural networks with two or more fully-connected, hidden layers, which are usually represented in a group of layers stacked linearly. CNNs are a special type of DNNs designed to learn local patterns in the data through convolution operations (filtering) in convolutional layers, which are then pooled in pooling layers to reduce the size of the representation and to compute the parameters faster. CNNs are optimized for image processing and commonly used in computer applications. RNNs are another type of DNNs specifically designed to work with sequence data. Unlike DNNs and CNNs, RNNs learn representations from data in an iterative manner, allowing the output of a layer to be used as the input to the same layer in the next time step. RNNs are usually defined by the type of recurrent layers used, with two common layers being Long Short-Term Memory (LSTM) and Gated Recurrent Unit.

Of the five models built in the four papers included in this review, two were DNN-based, two CNN-based, and one RNN-based (LSTM to be more precise). Coming from the same research group, the DNN models reported by [27] and [28] used the same network architecture, with three hidden
layers containing 128, 256, and 128 nodes, respectively. The classification accuracy of the DNN model was 98.02% in [27] and 99.12% in [28].

Despite being more commonly applied to image data for computer vision applications, CNNs have been used to analyze the sequence data obtained from the EEG device. The CNN model reported by [26] included three convolutional layers, one pooling layer, and two fully-connected layers. [27]’s CNN model was different in that it included three convolutional layers, one pooling layer, and one fully-connected layer. Of note, [27] converted the EEG signals into a black-and-white image before feeding the data into the network to better utilize the optimized performance of the CNN architecture for the analysis of image data. With this approach, [27] obtained a classification accuracy of 98.82%, whereas the accuracy of [26]’s CNN model was 87.13%.

The RNN model built by [29] was an RNN using LSTM with three time-steps and seven fully-connected hidden layers. The best classification accuracy of the LSTM model was 83.94% with a 60-second step. Given the optimized performance of RNNs on time-series data, the relatively poor performance of the LSTM model compared to the DNN and CNN architecture highlights the need for future research into this area. Due to the stark differences in experimental procedures across these studies (e.g., different EEG devices), no firm conclusions can be drawn in relation to the comparison of the performance of these three DL architectures when classifying cybersickness levels from EEG data. It is possible that the low accuracy rate of [29] can be attributed to the fact that the study used a single-channel wireless EEG devices, whereas an 8-channel scalp EEG device and 14-channel wireless EEG device were used in [26] and [27-28], respectively.

2) Activation Functions

Activation functions are crucial hyperparameters of DL architectures that determine the output of nodes and are used to introduce non-linearity to the computation of the output of a node. The most commonly-used activation function for hidden layers in DNN models and convolutional layers in CNN models was the rectified linear unit (ReLU) function, which was used in the four models reported in [27-29]. The activation function used in the CNN model reported by [26] was the leaky ReLU. As for the activation functions used for the output layer, all models used the sigmoid function. While these common choices usually work well for the type of classification tasks used in the prediction of cybersickness from EEG data, future research is warranted to compare different activation functions and identify the optimal combination(s) of these activation functions for cybersickness classification problems.

IV. DISCUSSION

This systematic review provided an analysis of the existing studies into the application of DL algorithms to the EEG-based detection of cybersickness experienced as a result of exposure to VR. As a result of the systematic search of scientific databases, we found only four papers investigating the EEG-based detection of cybersickness using DL frameworks, which clearly indicates the fact that research into this exciting area is in its infancy. The review indicated that these studies have all been recently published and that they have utilized similar procedures for the design, administration, and analysis of EEG-based VR experiments. In what follows, we provide some guidelines for future research into this area, highlighting trends and issues identified in the studies reviewed here.

A. Experimental Design

All four studies used similar experimental procedures in which users were exposed to a VR experience and then provided self-reported assessments of their cybersickness. This way authors were able to construct large datasets involving time-series EEG data as a 2D tensor of (timestamp x channel) shape for each participant. Based on the trend observed in these studies, future studies should consider using multiple, shorter VR experiences as opposed to a single, longer VR experience to collect more data samples. In so doing, each participant will provide multiple data samples, reducing the number of participants that need to be recruited for future experiments.

Another trend in the literature is to formulate the DL task as a binary classification in which the target variable indicates whether or not users experienced cybersickness during the VR experience. Only one out of the five DL models reported in these four studies have used multiclass classification [26], where users rated the severity of their cybersickness on a Likert scale. The rest of the studies used binary classification and had users make a dichotomous selection (cybersickness vs. not) [27-29]. None of the studies included in this review compared the effect of using binary classification to that of using multiclass classification on the performance of DL models when classifying cybersickness levels. That said, [30] did compare the two when classifying cybersickness based on some other physiological signals and found that binary classification yielded a classification accuracy of 82%, while the same was 56% for ternary classification (no, mild, and severe cybersickness). With multiclass classification, it is more likely to obtain an unbalanced dataset in terms of the distribution of the different categories of the target/class variable, especially when there is a limited number of users participating in the experiment. Therefore, for future studies, it would be prudent to obtain a balanced sample and start out with binary classification. As research into this area flourishes, it is projected that more studies comparing binary classification to multiclass classification will become available.

B. DL Architectures

Previous studies included in this review have built DNNs, CNNs, and RNNs to classify cybersickness from EEG
signals. The details of these frameworks are available in Table 2. While these studies clearly explained their models, the descriptions of these models can be improved in several ways, which serve as good guidelines for future studies. To begin with, data preprocessing steps should be clearly outlined in a separate section. This section should provide information on whether the EEG data were transformed to extract power signals or whether raw EEG values were used. If transformations and other feature extraction techniques were applied, these should be clearly explained and justified.

When reporting the structure of DL frameworks, the type of the DL model should be explicitly stated. The description of the DL architecture should clearly state the input formulation (the shape of the feature tensor), the number and type of layers, activation functions used in these layers, and the shape and activation function of the output layer. There should also be a detailed description of other model-specific key hyperparameters, such as filters and pooling layers applied to convolutional layers in CNNs and time steps for RNNs.

Future studies should also elaborately describe how they addressed the problem of overfitting, which occurs when the predictive model is very specific to the training data but cannot generalize to the test data and is even more pronounced for DL frameworks. Activity regularization, dropout, and early stopping are some common strategies to reduce overfitting. They should be used when necessary, and this should be explicitly described. Furthermore, future studies should clearly describe how the data were split into training, validation, and test sets, as well as the evaluation strategy (e.g., k-fold cross validation).

Another issue was that previous studies have solely relied on classification accuracy as a performance metric. Only [29] reported other metrics, such as a confusion matrix. While classification accuracy is extensively reported in the literature, it fails to capture the whole picture when it comes to evaluating the performance of a predictive model. Thus, future studies should report a wider array of classification metrics, such as confusion matrix, F-1 score, AUC-ROC, and log loss. It would also be useful to report training and prediction times for various models to enable other researchers to better assess the tradeoff between the accuracy and speed of these models.

C. Data and Code Sharing

One common issue across the studies included in this review was that none of them have made their data or code publicly available. Given the dire need for reproducible AI research in computer science circles [31], it is of paramount importance that studies conducting computational experiments, such as the ones included in this review, publicly share the data and code used for preprocessing and analysis. This simple open-science practice will enable future researchers to devise new data analysis strategies and help broaden the availability of studies into this exciting, but nascent, area of research, while at the same time increasing the credibility of scientific research in this field.

REFERENCES

[1] L. Rebenitsch, and C. Owen, “Review on cybersickness in applications and visual displays,” Vir. Real., vol. 20, pp. 101-125, 2016.
[2] R. S. Kennedy, J. Drexler, and R. C. Kennedy, “Research in visually induced motion sickness,” Applied Ergonomics, vol. 41, pp. 494-503, 2010.
[3] C. Yildirim, “Don’t make me sick: investigating the incidence of cybersickness in commercial virtual reality headsets,” Vir. Real., vol. 24, pp. 231-239, 2020.
[4] S. Davis, K. Nesbitt, and E. Naliavaiok, “A systematic review of cybersickness,” in: Proc. of the 2014 Conf. on Interactive Entertainment, pp. 1-9, 2014.
[5] C. Yildirim, “Cybersickness during VR gaming undermines game enjoyment: a mediation model,” Displays, vol. 59, pp. 35-43, 2019.
[6] J. E. Bos, W. Bles, and E. L. Groen, “A theory on visually induced motion sickness,” Displays, vol. 29, pp. 47-57, 2008.
[7] C. M. Oman, and C. M, “Motion sickness: a synthesis and evaluation of the sensory conflict theory,” Canadian J. of Physiol. and Pharmacol., vol. 68, pp. 294-303, 1990.
[8] R. S. Kennedy, N. E. Lane, K. S. Berbaum, and M. G. Lilienthal, “Simulator sickness questionnaire: an enhanced method for quantifying simulator sickness,” Int’l J. of Aviation Psych., vol. 3, pp. 203-220, 1993.
[9] M. S. Dennison, A. Z. Wisti, and M. D’Zmura, “Use of physiological signals to predict cybersickness,” Displays, vol. 44, pp. 42-52, 2016.
[10] A. Garcia-Agundez, C. Reuter, P. Caserman, R. Konrad, and S. Göbel, “Identifying cybersickness through heart rate variability alterations.” Int’l J. of Vir. Real. vol. 19, pp. 1-10, 2019.
[11] R. Islam, Y. Lee, M. Jaloli, I. Muhammad, D. Zhu, and J. Quarel, “Automatic Detection of Cybersickness from Physiological Signal in a Virtual Roller Coaster Simulation,” in: 2020 IEEE Conference on Virtual Reality and 3D User Interfaces Abstracts and Workshops (VRW), pp. 649-650.
[12] R. Islam, “A Deep Learning based Framework for Detecting and Reducing onset of Cybersickness,” in: 2020 IEEE Conference on Virtual Reality and 3D User Interfaces Abstracts and Workshops (VRW), pp. 559-560, 2020.
[13] R. Liu, , M. Xu, Y. Zhang, E. Peli, and A. D. Hwang, “A Pilot Study on Electroencephalogram-based Evaluation of Visually Induced Motion Sickness,” J of Imaging Sci. and Tech., vol. 64, pp. 20501-10, 2020.
[14] U. Celikcan, “Detection and Mitigation of Cybersickness via EEG-Based Visual Comfort Improvement.” In: 2019 3rd International Symposium on Multidisciplinary Studies and Innovative Technologies (ISMSIT), pp. 1-4, 2019.
[15] S. W. Chuang, C. H. Chuang, Y. H. Yu, J. T. King, and C. T. Lin, “EEG alpha and gamma modulators mediate motion sickness-related spectral responses,” Int’l J. of Neural Systems, vol. 26, 2016.
[16] J. Heo, and Y. Gilwon, “EEG studies on physical discomforts induced by virtual reality gaming.”J. of Electrical Engineering & Tech., vol. 15, pp. 1323–1329, 2020.
[17] L. W. Ko, C. S. Wei, T. P. Jung, and C. T. Lin, “Estimating the level of motion sickness based on EEG spectra.” in: Int’l Conf. on Foundations of Augmented Cognition, pp. 169-176, 2011.
[18] Y. C. Chen, J. R. Duann, C. L. Lin, S. W. Chuang, T. P. Jung, and C. T. Lin, “Motion-sickness related brain areas and EEG power activates,” in: Int’l Conf. on Foundations of Augmented Cognition, pp. 348-354, 2009.
[19] Y. C. Chen, J. R. Duann, S. W. Chuang, C. L. Lin, L. W. Ko, T. P. Jung, and C. T. Lin, “Spatial and temporal EEG dynamics of motion sickness,” Neuroimaging, vol. 49, pp. 2862-2870, 2010.
[20] M. A. Mawalid, A. Z. Khoirunnisa, M. H. Purnomo, and A. D. Wibawa, “Classification of EEG Signal for Detecting Cybersickness through Time Domain Feature Extraction using Naïve Bayes,” in: 2018 International Conference on Computer Engineering, Network and Intelligent Multimedia (CENIM), pp. 29-34, 2018.

[21] C. T. Lin, S. F. Tsai, and L. W. Ko, “EEG-based learning system for online motion sickness level estimation in a dynamic vehicle environment,” IEEE transactions on neural networks and learning systems, vol. 24, pp. 1689-1700, 2013.

[22] L. W. Ko, H. C. Lee, S. F. Tsai, T. C. Shih, Y. T. Chuang, H. L. Huang, ..., and C. T. Lin, “EEG-based motion sickness classification system with genetic feature selection,” in: 2013 IEEE Symposium on Computational Intelligence, Cognitive Algorithms, Mind, and Brain (CCMB), pp. 158-164, 2013.

[23] E. S. Pane, A. Z. Khoirunnisa, A. D. Wibawa, and M. H. Purnomo, “Identifying severity level of cybersickness from eeg signals using cn2 rule induction algorithm,” in: 2018 International Conference on Intelligent Informatics and Biomedical Sciences (ICIIBMS), pp. 170-176, 2018.

[24] M. Dennison Jr, M. D’Zmura, A. Harrison, M. Lee, and A. Raglin, “Improving motion sickness severity classification through multimodal data fusion,” in: Artificial Intelligence and Machine Learning for Multi-Domain Operations Applications, p. 110060, 2019.

[25] X. Li, C. Zhu, C. Xu, J. Zhu, Y. Li, and S. Wu, “VR motion sickness recognition by using EEG rhythm energy ratio based on wavelet packet transform,” Computer Methods and Programs in Biomedicine, vol. 188, pp. 105266, 2020.

[26] J. Kim, W. Kim, H. Oh, S. Lee, and S. Lee, “A deep cybersickness predictor based on brain signal analysis for virtual reality contents,” in: Proceedings of the IEEE International Conference on Computer Vision, pp. 10580-10589, 2019.

[27] D. Jeong, S. Yoo, and J. Yun. “Cybersickness analysis with eeg using deep learning algorithms,” in: 2019 IEEE Conference on Virtual Reality and 3D User Interfaces (VR), pp. 827-835, 2019.

[28] D. Jeong, S. Yoo, and J. Yun. “VR sickness measurement with EEG using DNN algorithm,” in: Proceedings of the 24th ACM Symposium on Virtual Reality Software and Technology, pp. 1-2, 2018.

[29] C. Y. Liao, S. K. Tai, and R. C. Chen. “Using EEG and Deep Learning to Predict Motion Sickness Under Wearing a Virtual Reality Device.” IEEE Access, vol. 8, pp. 126784-126796, 2020.

[30] A. Garcia-Agundez, C. Reuter, H. Becker, R. Konrad, P. Caserman, A. Miede, and S. Göbel, “Development of a classifier to determine factors causing cybersickness in virtual reality environments,” Games for Health J., vol. 8, pp. 439-444, 2019.

[31] O. E. Gundersen, Y. Gil, and D. W. Aha, “On reproducible AI: Towards reproducible research, open science, and digital scholarship in AI publications,” AI magazine, vol. 389, pp. 56-68, 2018.