Research Article

Corrosion Evaluation of Pure Mg Coated by Fluorination in 0.1M Fluoride Electrolyte

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In the ongoing research on the application of biodegradable materials, surface treatment of is considered to be a relatively effective solution to the excessive degradation rates of Mg alloys. In this study, to further optimize the proven effective surface coatings of fluoride, a low-voltage preparation fluorination method was used to achieve coating effectiveness under safer conditions. Optical observation, scanning electron microscopy (SEM), X-ray diffraction (XRD), energy-dispersive spectroscopy (EDS), and potential dynamic polarization (PDP) experiments were used for the analysis and evaluation. The coating characteristics of the MgF2 coatings treated in the 10–90 V voltage range, including the structure, chemical conformation, and electrochemical corrosion assessment, were fully defined. The anodic fluoridation results showed that a pore structure of 1–14 μm thickness was formed on the Mg alloy substrate, and the coating was composed of Mg fluoride. The results of immersion corrosion and electrochemical corrosion experiments showed that compared with pure Mg, anodic fluorinated samples below 40 V exhibited better corrosion resistance, the prepared MgF2 coating was more uniform, and the surface mostly exhibited point corrosion. When the voltage reached or exceeded 60 V, the prepared coating exhibited poor corrosion resistance, fracture, and protrusions. After corrosion, it mostly exhibited surface corrosion. The results indicate that idealized coatings can be obtained at relatively low and safe voltage ranges. This finding may enable more economical, environmentally friendly, and safe preparation of coatings.

1. Introduction

Mg alloys have been continuously studied in the field of biodegradable materials, because Mg and Mg alloys are the most clinically useful restorative materials owing to their excellent dimensional stability and mechanical properties [1], as well as their reduced potential for stress shielding [2]. Previous studies have discussed both permanent and nonpermanent material designs. In this regard, potential complications and risks of reoperation can be avoided if nonpermanent materials, that is, biodegradable materials, are used [3, 4]. Thus, Mg has been applied in various fields, including biochemistry and materials science [5]. In addition, Mg functions as a cofactor of adenosine triphosphate, induces osteogenesis, and synergizes biocircadian expression, demonstrating its potential as an implant material [6, 7].

However, pure Mg has a limitation for its clinical application and research, which is the fast decomposition rate in humoral situations and the inappropriate corrosion processes that can produce some adverse effects [4, 8–10]. Thus, methods to modulate the dissolution rate of early Mg alloy anodes are required. Therefore, the main objective of our study was to reduce the degradation rate of Mg alloys in a simulated body fluid environment.

Typically, methods to coordinate the alloy corroding behavior include electroplating and surface passivation [11–13]. In addition, ceramic coatings are also effective [14, 15]. By analyzing existing studies, we chose to further optimize
the feasibility of the existing fluorination coating treatment [16]. In this treatment, the corrosion conditions and corrosion rates are regulated by insulating the metal from external influences through insoluble corrosion-resistant substances. The metal oxide film formed also has electronic properties such as semiconduction and insulation [17].

Anodization allows the thickness and structure of the prepared coating to be controlled by varying the voltage. However, the prepared Mg oxide coatings can be affected by surface fracture and corrosion resistance [18, 19]. Micro-arc fluorination (MAF) is a combination of anodic oxidation and fluorination, using high voltage to form a layer of MgF₂ coating on the sample surface in a fluorinated environment [19–23]. However, the preparation process generates large quantities of hydrogen fluoride gas, which is harmful to humans and causes environmental pollution. Conventional MAF methods generally use voltages above 100 V and high concentrations of hydrofluoric acid [24]. Therefore, this experiment attempted to use a solution with a low fluoride ion concentration as the electrolyte and conduct anodic fluorination (AF) in a lower voltage range. Low-pressure coatings are more environmentally friendly and economical than high-pressure coatings. This reduces the release of irritating fumes, pollution and environmental damage, and harm to humans. The AF process requires a short time. Uniformly dense films can be prepared during this process, and pores are formed. The density of the films is similar to that of bone tissue and has been proven to be highly biocompatible [18, 21–23]. Moreover, the thicknesses of the MgF₂ coatings prepared under different voltages are different, which is more conducive to cell attachment and subsequent preparation [25, 26]. MgF₂ has strong corrosion resistance in vitro and can maintain good clinical effects after implantation in the human body [18, 25, 27–29].

In this experiment, the AF technique was used to prepare MgF₂ ceramic coatings on Mg surfaces. In the fluoride electrolyte (0.1 mol/L NH₄HF₂), the coating preparation experiment was performed in the voltage range of 10–90 V. Scanning electron microscopy (SEM) was used to measure the surface morphology of the coating, and potential dynamic polarization (PDP) was used to measure the electrochemical corrosion. The fluorine content of the sample surface under different voltages was analyzed, and the corrosion resistance of the prepared sample in Hank’s balanced salt solution (HBSS) was analyzed and evaluated.

### 2. Materials and Methods

#### 2.1. Sample Preparation

Pure Mg (Dongguan FeiTai Metal Products Co., Ltd., China) was cut into pieces with dimensions of 20 × 20 × 3 mm. The samples were polished with grade 1200 SiC paper in absolute ethyl alcohol. Then, they were rinsed with absolute ethyl alcohol and blow-dried.

#### 2.2. Surface Modification

The samples were divided into eight groups and then separately placed in 10, 20, 30, 40, 50, 60, 70, 80, and 90 V electrolytic cells for 3 min as the anode, and a graphite rod was chosen as the cathode. A magnetic bar was chosen to stir the electrolytic solution, which was a solution of 0.1 mol/L NH₄HF₂. The progress of the AF is shown in Figure 1. The samples were then washed with distilled water and dried. The conditions of the surface treatment are listed in Table 1.

#### 2.3. Surface Characterization

The surface morphologies of the samples and cross-sectional images were observed using a scanning electron microscope (JSM-67000). The elementary compositions were then determined by energy-dispersive spectroscopy (EDS). X-ray diffraction (XRD) measurements of the Mg phase on the surface of the MgF₂ sample were also performed at a scan rate of 1°/min at 40 kV and 30 mA.

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**Figure 1: Diagram of AF of pure Mg.**

**Table 1: Sample codes and surface treatment conditions.**

| Sample code | Treatment conditions | Treatment time (min) |
|-------------|----------------------|---------------------|
| Pure Mg     | /                    | /                   |
| AF10        | Anodizing by DC* power supply in 10 V | 3             |
| AF20        | Anodizing by DC power supply in 20 V | 3             |
| AF30        | Anodizing by DC power supply in 30 V | 3             |
| AF40        | Anodizing by DC power supply in 40 V | 3             |
| AF50        | Anodizing by DC power supply in 50 V | 3             |
| AF60        | Anodizing by DC power supply in 60 V | 3             |
| AF70        | Anodizing by DC power supply in 70 V | 3             |
| AF80        | Anodizing by DC power supply in 80 V | 3             |
| AF90        | Anodizing by DC power supply in 90 V | 3             |

*DC: direct current.
2.4. Corrosion Resistance Test. In the immersion corrosion experiment, all processed samples were vertically immersed in the HBSS and kept at 37°C for seven days. For the sample surface area, the volume ratio of HBSS was 20 mL/cm², as per the ASTM standard G31. After seven days, the samples were rinsed with absolute ethanol and blow-dried, and electronic pictures were taken.

2.5. Electrochemical Corrosion Test. The exposed fluorinated Mg alloy surface was set to 1 cm². Electrochemical corrosion tests were performed using the PDP method with a constant potentiostat (VersaSTAT 3:300) and analyzed using a commercial software (VersaStudio 2.44.4). The classic three-electrode battery consisted of a working electrode for the test sample, a pure platinum rod electrode, and Ag/AgCl/Sat-KCl as the reference electrode (+197 mV compared with a standard hydrogen electrode). HBSS (1000 mL, WELGENE Inc., Korea) was used as an electrolyte and placed in a double-walled beaker, with the temperature maintained at 37 ± 1°C at all times. The scanning rate of the PDP measurements was 3 mV/s.

3. Results and Discussion

The surface condition of pure Mg coated by AF can be visually observed in Figure 2. The coating was more uniform before AF50, as shown in Figures 2(b)–2(f). However, there was a large area of coating shedding off the surface at AF50, and different degrees of coating flaring can be found at the shedding junction. The surface topography also became rougher with increasing voltage in the subsequent coating.

Figure 3 shows the varied microscopic surface morphologies of the samples treated at different voltages under SEM. The AF coating started to form at 10 V, and the coating exhibited a dot-like morphology. The AF20 coating appeared more uniformly covered, but the thickness of the coating was
The coatings of AF30 and AF40 gradually exhibited a homogeneous matte-like appearance. The coating of AF50 was more differentiated compared to those of AF40 and the previous treatment group. As shown in Figure 3(f), AF50 formed a coating with an inhomogeneous, nondense, and coral-like surface appearance. As the voltage increased, the coral-like shape became coarser and shale-like. The effect of voltage on surface morphology was evident. The surface microstructure was conducive to tissue attachment [30, 31].

The surface morphology of the fluorinated coating prepared in this experiment was slightly similar to that of the microarc oxidation coating, and we speculate that the microgaps and micropores produced on the surface were due to the plasma discharge and the involvement of a small amount of electrolyte particles in the electrolysis [19].

Figure 4 shows the fluoride coating produced on the surface of pure Mg analyzed by EDS. The results show that the F and Mg peaks appeared under different voltages. The main component of the surface coating on the AF sample was MgF2. The percentage of elemental fluorine in the coating varied with voltage from pure Mg to 60 V treated samples. The increment in the elemental fluorine content peaked at the 60 V treatment condition, with a 48.28% increase compared to that of the AF10 voltage. The fluorine contents on the surfaces of AF70, AF80, and AF90 were 52.54%, 51.66%, and 53.12%, respectively.

Figure 5 shows the SEM cross-sectional morphology of the anodic fluorinated Mg, from which it can be seen that the thickness of the coatings thickened with increasing voltage [17]. The good adhesion of the coating to the Mg substrate without any separation boundary was due to the chemical transformation of the AF coating to the Mg substrate [19].

Figure 6 shows the relationships among the coating thickness, mass, atomic ratio, and voltages obtained from the EDS analysis plotted as a graph. The horizontal axis, left vertical axis, and right vertical axis are the voltage, coating thickness, and fluorine mass to atom ratio, respectively. From the figure, it can be clearly seen that the mass and atomic proportion curves show high consistency as the voltage increases. In the voltage range of 30–50 V, the mass and atomic proportion curves increased at the fastest speed and reached a maximum after 60 V. Because the coating thickness curve rapidly increased after 50 V, EDS X-rays were unable to penetrate the coating and scan for pure Mg, resulting in no significant increase in the mass curve of fluorine and atomic proportion curve. We speculate that the sudden decrease in the AF90 coating thickness may be due to the coating shedding that occurred during the coating preparation process. This also indicates that several microgaps and micropores formed inside the coating at 90 V, which caused the coating structure to be slightly loose and easy to peel off [19].
Figure 4: Continued.
Figure 7 shows the XRD patterns of the pure Mg and MgF₂ samples. Simultaneously, the crystal structure of the sample surface was analyzed. Compared to the untreated pure Mg, the diffraction pattern of Mg fluoride clearly showed the presence of MgF₂. As seen in the figure, AF10, AF20, AF30, and AF40 were basically the same in terms of the number of diffraction peaks, angular position, and shape of the diffraction peaks, whereas there were differences in the diffraction patterns of AF50, AF60, AF70, AF80, and AF90. This may be attributed to the change in coating thickness. However, there was only one crystalline phase from AF10 to AF90, which may be because the other crystalline phases were too small or amorphous, as reflected by the XRD analysis [32]. XRD requires a certain thickness of material to be measured to obtain a clear diffraction peak of the sample in the diffraction pattern.

To comprehensively and accurately evaluate the corrosion resistance of specimens, it is essential to conduct an electrochemical test on the fluoride-treated object and the control group (pure Mg) [11]. Figure 8 shows the Tafel curves of the samples. The polarization test is an electrochemical method that reflects the corrosion resistance properties by the metal corrosion potential ($E_{corr}$) and corrosion current density ($I_d$). More corrosion-resistant states occur at lower current densities and at relatively high corrosion voltages [2].

As shown in Figure 8, the pure samples exhibited normal corrosion conditions. Therefore, considering the pure Mg characteristics as the evaluation criterion ($I_d$ pure Mg $2.25 \times 10^{-5}$ A/cm²), the electrochemical results were broadly divided into two groups. One group exhibited higher overall current density than the pure Mg (AF50–90, $I_d$ values of $2.61 \times 10^{-5}$, $3.83 \times 10^{-5}$, $8.55 \times 10^{-5}$, $6.98 \times 10^{-5}$, and $7.72 \times 10^{-5}$ A/cm², respectively), indicating poorer corrosion resistance, which suggests that the coating does not exhibit corrosion resistance effectiveness. On the contrary, the other
group exhibited resistance against corrosion, with \( I_d \) values of AF20 \( 4.13 \times 10^{-6} \), AF10 \( 6.37 \times 10^{-6} \), and AF30 \( 7.15 \times 10^{-6} \) A/cm², respectively. Corrosion resistance properties were not obtained at 40 V and higher voltage treatments. However, lower voltages, for example 30 V and below, optimized the corrosion resistance of Mg.
Therefore, a better coating impedance effect occurs in the relatively low-voltage experimental conditions, which is in agreement with the experimental expectations. Moreover, in the low-voltage treatment group, the corrosion resistance was more prominent for AF10, AF30, and AF20 (ranked from highest to lowest). A minimum current density and a relatively high corrosion voltage were obtained for the 10 V treatment sample.

Gu et al. [21] reported that the corrosion resistance of oxide coatings can be modulated by controlling the voltage applied during the coating preparation process. This was confirmed in the present study. In contrast to previous studies [16, 17], in the present experiments, reaction conditions in the safe voltage range were used to prepare coatings with tunable corrosion rates. This further confirms that the application of AF technology to Mg alloy coatings is still promising and valuable for research.

In combination with the SEM results, the fluoride coatings at 50 V and higher showed chipping or spalling, a phenomenon that may lead to uneven distribution under

**Figure 7**: XRD patterns of pure Mg, AF10, AF20, AF30, AF40, AF50, AF60, AF70, AF80, and AF90.

**Figure 8**: Electrochemical corrosion results: pure Mg, AF10, AF20, AF30, AF40, AF50, AF60, AF70, AF80, and AF90.
optical observation. According to Hornberger et al., for coating samples, corrosion may start with some defects in the coating, which are nonuniform in nature [33, 34]. Figure 9 shows the optical observation of each group of samples after 7 days of HBSS immersion and etching. During the degradation of the coating, MgF₂ dissolved into F⁻ and Mg²⁺, and the latter reacted with OH⁻ to produce Mg(OH)₂ deposits. A layer of Mg(OH)₂ degradation products covered the sample. Owing to the lower solubility of MgF₂, Mg(OH)₂ was generated at a slower rate, and the coating exhibited better corrosion resistance. As corrosion proceeded, H₂O and Cl⁻ penetrated the Mg alloy matrix, and the Mg alloy started to degrade to form Mg(OH)₂ and H₂ [35]. Owing to the absence of acid cleaning, grey-blue surface corrosion product deposits can be observed. Looking at the sediment distribution, we found more uniform observations and a smaller proportion of product distribution in AF20. AF50–AF90 exhibited large product deposits with similar moisture-shedding patterns.

4. Conclusion

In this study, under AF treatment, the following conclusions were drawn:

1. After AF treatment, the surface formed coral-like and shale-like surface morphologies
2. XRD and EDS analyses indicated that the main component of the surface coatings formed by AF was MgF₂
3. Within a certain range, the thickness of the coating increased with an increase in voltage and reached a peak at AF60
4. Compared with the untreated samples, the corrosion resistance of the treated samples was improved. The samples treated at 10 V were more resistant to corrosion

Figure 9: Optical observations of each group of samples after immersion experiments of (a) pure Mg, (b) AF10, (c) AF20, (d) AF30, (e) AF40, (f) AF50, (g) AF60, (h) AF70, (i) AF80, and (j) AF90.
Data Availability

The data used to support findings of this study are included within the article.

Conflicts of Interest

We declare that we have no financial or personal relationships with other people or organizations that can inappropriately influence our work.

Authors’ Contributions

Chun Yu Dai, and Xinzhe Gao did the conceptualization, methodology, formal analysis, investigation, and writing of original draft. ChuanYao Zhai did the methodology, validation, writing—review and editing, and visualization. Bing Cheng Zhao did the validation, data curation, writing—review and editing, Qi Jia and HaoYu Shi did the writing. ChunYao Zhai did the methodology, validation, resources, supervision, project administration, and funding acquisition. Chun Yu Dai, Xinzhe Gao, and ChuanYao Zhai contributed equally to this work.

References

[1] Y. Su, J. Lin, Y. Su, W. Zai, G. Li, and C. Wen, "Investigation on composition, mechanical properties, and corrosion resistance of Mg-0.5Ca-X(Sr, Zr, Sn) biological alloy," Scanning, vol. 2018, Article ID 6519310, 10 pages, 2018.

[2] N. Hort, Y. Huang, D. Fechner et al., "Magnesium alloys as implant materials - principles of property design for Mg-RE alloys," Acta Biomaterialia, vol. 6, no. 5, pp. 1714–1725, 2010.

[3] G. Wang, X. Xiong, D. Xie et al., "A scalable approach for dendrite-free alkali metal anodes via room-temperature facile surface fluorination," ACS Applied Materials & Interfaces, vol. 11, no. 5, pp. 4962–4968, 2019.

[4] F. Witte, "The history of biodegradable magnesium implants: a review," Acta Biomaterialia, vol. 6, no. 5, pp. 1680–1692, 2010.

[5] C. Liu, Z. Ren, Y. Xu, S. Pang, X. Zhao, and Y. Zhao, "Biodegradable magnesium alloys developed as bone repair materials: a review," Scanning, vol. 2018, Article ID 9216314, 15 pages, 2018.

[6] K. A. Feehey, L. L. Hansen, M. Putker et al., "Daily magnesium fluxes regulate cellular timekeeping and energy balance," Nature, vol. 532, no. 7599, pp. 375–379, 2016.

[7] Z. J. Li, X. Gu, S. Lou, and Y. Zheng, "The development of binary Mg-Ca alloys for use as biodegradable materials within bone," Biomaterials, vol. 29, no. 10, pp. 1329–1344, 2008.

[8] R. C. Zeng, W. Dietzel, F. Witte, N. Hort, and C. Blawert, "Progress and challenge for magnesium alloys as biomaterials," Advanced Engineering Materials, vol. 10, no. 8, pp. B3–B14, 2008.

[9] Z. Zhen, X. Liu, T. Huang, T. F. Xi, and Y. Zheng, "Hemolysis and cytotoxicity mechanisms of biodegradable magnesium and its alloys," Materials Science & Engineering C-Materials for Biological Applications, vol. 46, pp. 202–206, 2015.

[10] J. Hofstetter, E. Martinelli, A. M. Weinberg et al., “Assessing the degradation performance of ultrahigh-purity magnesium _in vitro_ and _in vivo_,” Corrosion Science, vol. 91, pp. 29–36, 2015.

[11] X. M. Xiong, Y. Yang, J. Li et al., "Research on the microstructure and properties of a multi-pass friction stir processed 6061Al coating for AZ31 mg alloy," Journal of Magnesium and Alloys, vol. 7, no. 4, pp. 696–706, 2019.

[12] T. S. N. Sankara Narayanan, I. S. Park, and M. H. Lee, "Strategies to improve the corrosion resistance of microarc oxidation (MAO) coated magnesium alloys for degradable implants: prospects and challenges," Progress in Materials Science, vol. 60, pp. 1–71, 2014.

[13] X. du, Y. Song, X. Xuan et al., "Characterization of a bioreabsorbable magnesium-reinforced PLA-integrated GTR/GBR membrane as dental applications," Scanning, vol. 2020, Article ID 6743195, 10 pages, 2020.

[14] X. L. Fan, Y. F. Huo, C. Y. Li et al., "Corrosion resistance of nanostructured magnesium hydroxide coating on magnesium alloy AZ31: influence of EDTA," Rare Metals, vol. 38, no. 6, article 1216, pp. 520–531, 2019.

[15] Y. Su, Y. Su, W. Zai, G. Li, and C. Wen, "In vitro degradation behaviors of manganese-calcium phosphate coatings on an Mg-Ca-Zn alloy," Scanning, vol. 2018, Article ID 6268579, 9 pages, 2018.

[16] H. B. Jiang, G. Wu, S. B. Lee, and K. M. Kim, "Achieving controllable degradation of a biomedical magnesium alloy by anodizing in molten ammonium bifluoride," Surface & Coatings Technology, vol. 313, pp. 282–287, 2017.

[17] H. B. Jiang, Y. K. Kim, J. H. Ji, I. S. Park, T. S. Bae, and M. H. Lee, "Surface modification of anodized Mg in ammonium hydrogen fluoride by various voltages," Surface & Coatings Technology, vol. 259, pp. 310–317, 2014.

[18] T. T. Yan, L. Tan, B. Zhang, and K. Yang, "Fluoride conversion coating on biodegradable AZ31B magnesium alloy," Journal of Materials Science & Technology, vol. 30, no. 7, pp. 666–674, 2014.

[19] Y. H. Gu, S. Bandopadhyay, C. F. Chen, C. Ning, and Y. Guo, "Long-term corrosion inhibition mechanism of microarc oxidation coated AZ31 Mg alloys for biomedical applications," Materials & Design, vol. 46, pp. 66–75, 2013.

[20] Q. M. Zhao, X. Guo, X. Dang, J. Hao, J. Lai, and K. Wang, "Preparation and properties of composite MAO/ECID coatings on magnesium alloy," Colloids and Surfaces B-Biointerfaces, vol. 102, pp. 321–326, 2013.

[21] X. N. Gu, N. Li, W. R. Zhou et al., "Corrosion resistance and surface biocompatibility of a microarc oxidation coating on a Mg-Ca alloy," Acta Biomaterialia, vol. 7, no. 4, pp. 1880–1889, 2011.

[22] H. X. Guo, Y. Ma, J. S. Wang, Y. S. Wang, H. R. Dong, and Y. HAO, "Corrosion behavior of micro-arc oxidation coating on AZ91D magnesium alloy in NaCl solutions with different concentrations," Transactions of Nonferrous Metals Society of China, vol. 22, no. 7, pp. 1786–1793, 2012.

[23] L. C. Zhao, C. Cui, Q. Wang, and S. Bu, "Growth characteristics and corrosion resistance of micro-arc oxidation coating on pure magnesium for biomedical applications," Corrosion Science, vol. 52, no. 7, pp. 2228–2234, 2010.

[24] L. Sun, B. C. Zhao, T. Wang et al., "Surface characterization and corrosion resistance of biomedical AZ31 Mg alloy treated by microarc fluorination," Scanning, vol. 2020, Article ID 5936789, 15 pages, 2020.
[25] L. Mao, G. Yuan, J. Niu, Y. Zong, and W. Ding, “In vitro degradation behavior and biocompatibility of Mg-Nd-Zn-Zr alloy by hydrofluoric acid treatment,” Materials Science & Engineering C-Materials for Biological Applications, vol. 33, no. 1, pp. 242–250, 2013.

[26] X. L. Liu, Z. Zhen, J. Liu et al., “Multifunctional MgF₂/polydopamine coating on Mg alloy for vascular stent application,” Journal of Materials Science & Technology, vol. 31, no. 7, pp. 733–743, 2015.

[27] T. T. Yan, L. Tan, D. Xiong, X. Liu, B. Zhang, and K. Yang, “Fluoride treatment and in vitro corrosion behavior of an AZ31B magnesium alloy,” Materials Science & Engineering C-Materials for Biological Applications, vol. 30, no. 5, pp. 740–748, 2010.

[28] F. Witte, J. Fischer, J. Nellesen et al., “In vivo corrosion and corrosion protection of magnesium alloy LAE442,” Acta Biomaterialia, vol. 6, no. 5, pp. 1792–1799, 2010.

[29] S. Fintová, J. Drábiková, F. Pastorek et al., “Improvement of electrochemical corrosion characteristics of AZ61 magnesium alloy with unconventional fluoride conversion coatings,” Surface & Coatings Technology, vol. 357, pp. 638–650, 2019.

[30] W. W. Song, J. H. Heo, J. H. Lee, Y. M. Park, and Y. D. Kim, “Osseointegration of magnesium-incorporated sand-blasted acid-etched implant in the dog mandible: resonance frequency measurements and histomorphometric analysis,” Tissue Engineering and Regenerative Medicine, vol. 13, no. 2, pp. 191–199, 2016.

[31] Y.-J. Lee, Y. Kim, J. Y. Kim, J. B. Huh, M. R. Kim, and S. J. Kim, “Effect of different concentrations of Escherichia Coli-derived rhBMP-2 coating on osseointegration of implants in dogs,” Tissue Engineering and Regenerative Medicine, vol. 9, no. 4, pp. 209–215, 2012.

[32] K. Y. Chiu, M. H. Wong, F. T. Cheng, and H. C. Man, “Characterization and corrosion studies of fluoride conversion coating on degradable Mg implants,” Surface & Coatings Technology, vol. 202, no. 3, pp. 590–598, 2007.

[33] H. Hornberger, S. Virtanen, and A. R. Boccaccini, “Biomedical coatings on magnesium alloys - a review,” Acta Biomaterialia, vol. 8, no. 7, pp. 2442–2455, 2012.

[34] Q. Li, P. Zhu, S. Chen, B. Zhang, and K. Yang, “In vitro study on degradation of AZ31B magnesium alloy with fluoride conversion coating,” Materials Technology, vol. 32, no. 7, pp. 409–414, 2016.

[35] Z. Z. Li, Z. Ba, T. Wang, J. Kuang, and Y. Jia, “Fabrication and characterization of Mg-Mn hydrotalcite films on pure Mg substrates,” Materials Research Express, vol. 6, no. 11, p. 116440, 2019.