Hydrodynamic effects in the capture of rod-like molecules by a nanopore

Radost Waszkiewicz and Maciej Lisicki

Institute of Theoretical Physics, Faculty of Physics, University of Warsaw, Poland

E-mail: mklis@fuw.edu.pl and rwaszkiewicz@fuw.edu.pl

Received 30 September 2020, revised 30 November 2020
Accepted for publication 7 December 2020
Published 23 December 2020

Abstract

In the approach of biomolecules to a nanopore, it is essential to capture the effects of hydrodynamic anisotropy of the molecules and the near-wall hydrodynamic interactions which hinder their diffusion. We present a detailed theoretical analysis of the behaviour of a rod-like molecule attracted electrostatically by a charged nanopore. We first estimate the time scales corresponding to Brownian and electrostatic translations and reorientation. We find that Brownian motion becomes negligible at distances within the pore capture radius, and numerically determine the trajectories of the nano-rod in this region to explore the effects of anisotropic mobility. This allows us to determine the range of directions from the pore in which hydrodynamic interactions with the boundary shape the approach dynamics and need to be accounted for in detailed modelling.

Keywords: diffusion, nanopore, hydrodynamic interactions, hydrodynamic mobility

Some figures may appear in colour only in the online journal

1. Introduction

Nanopore sequencing is now a well-established technique for the determination of structure of biomolecules [1, 2], such as DNA [3], RNA [4], or proteins [5]. The molecules, which are typically slender filaments, are electrophoretically transported to the nanopore and then translocated through an orifice. The process of passage or threading, controlled by a combination of electric [6, 7], electrokinetic [8], entropic [9], osmotic [10, 11] and mechanical forces [12], is now well understood and explored.

However, the approach to the pore is described in less detail. Available models characterise the dynamics of the molecule by its diffusion coefficient \( D \) and electrophoretic mobility \( \mu_e \). This simplified approach has proved useful to establish the general properties of the system. In reference [13], Grosberg and Rabin determined the concentration of DNA near the pore using the Smoluchowski equation formalism. Qiao et al defined the capture radius of the pore [14], being the distance at which thermal fluctuations become comparable to the electrostatic potential energy, which bounds the region of attraction of the pore. In the following works, they extended this notion by introducing the orientational capture radius [15], being the range at which the electric field strongly orients the colloidal rods. These models, however, neglect the anisotropy of the particles, and of the hydrodynamic interactions with the wall which hinder diffusion at close distances. Hydrodynamic effects are known to alter the trajectories of close sedimenting particles [16, 17] by coupling to their inherent shape anisotropy and lead to a general slow-down of colloidal dynamics [18].

In this contribution, we fill this gap by formulating a detailed theoretical approach which accounts for anisotropic diffusivity of a model nano-rod both due to its non-isotropic shape and due to the particle-wall flow-mediated interactions. We first use this model to determine the time scales corresponding to the subsequent phases of motion of a nano-rod approaching a pore: purely Brownian motion far from the pore, electric field-induced translation and reorientation, and the wall influence region. Then we provide a quantitative insight by solving the equations of motion numerically for a collection of initial positions and orientation. We describe the resulting trajectories and mechanisms shaping the motion. This allows us to determine the wall influence region.
We focus on microparticles which can be modelled as stiff rods. This is appropriate for biomolecules of length $L$ shorter than their persistence length $L_p$. Examples of such nano-rods include dsDNA shorter than $L_p \approx 50$ nm (or ca 150 bp) or fd-viruses [19], with $L = 880$ nm and $L_p = 2.8 \mu$m, translocating through solid-state pores [20]. For longer molecules, the effects of elasticity and changing conformation can lead to coiling [21] or knotting [12, 22] and must be taken into account for proper modelling.

The paper is organised as follows. First, we describe the general model in section 2.1, specifying the form of electrostatic interactions in section 2.2 and hydrodynamic interactions in section 2.3. The following section 3 presents our results, divided into scaling insights in section 3.1, and a numerical analysis of the trajectories in section 3.2. We summarise our conclusions in section 4.

2. Model

2.1. Motion of the nanorod

We consider an ellipsoidal rod of length $L$ with its centre located at a point $r$, as sketched in figure 1. The aspect ratio of the rod is $p = 10$. The director of the rod is a unit vector $u$. The nanopore is at the centre of a Cartesian lab coordinate system, with the $z$ axis being normal to the wall, defined by the $xy$ plane. Thus, the rod is at a distance $H = r \cdot e$, from the wall and its inclination angle $\theta$ is determined by $\cos \theta = u \cdot e_z$.

The rod is charged and moving in an electric field generated by the nanopore. The field exerts an electrostatic force, $F_e$, and torque, $T_e$, on the rod. On the other hand, the suspending fluid reacts to the motion of the particle by exerting a frictional force, $F_h$, and torque, $T_h$. Because the flow is characterised by a small Reynolds number, the lack of inertia yields the following equations of motion of the particle

$$F_e + F_h = 0,$$

$$T_e + T_h = 0,$$

which determine the translational and rotational velocity of the particle, $V$ and $\Omega$, respectively. These are then used to evaluate the trajectory and orientation according to

$$\frac{\partial r}{\partial t} = V,$$

$$\frac{\partial u}{\partial t} = \Omega \times u.$$
related to its translational and angular velocities, $V$ and $\Omega$, via the friction (or resistance) tensor [23, 24]

$$\begin{pmatrix} F_t \\ T_r \end{pmatrix} = - \begin{pmatrix} \zeta^u \\ \zeta^r \end{pmatrix} \begin{pmatrix} \zeta^{ur} \\ \zeta^{ru} \end{pmatrix} \begin{pmatrix} V \\ \Omega \end{pmatrix}. \tag{10}$$

The indices $tt$ and $rr$ above denote the translational and rotational parts, respectively, while the tensors $\zeta^u$ and $\zeta^r$ describe the translation–rotation coupling.

If a particle is moving under the action of a known force and torque, a complementary problem is formulated using the mobility tensor $\mu$ which is an inverse of the friction tensor

$$\mu = \begin{pmatrix} \mu^u \\ \mu^r \end{pmatrix} = \begin{pmatrix} \zeta^{ur} \\ \zeta^{ru} \end{pmatrix}^{-1} = \zeta^{-1}. \tag{11}$$

Finally, the mobility tensor is related to the diffusion matrix $D$ by the fluctuation–dissipation theorem

$$D = k_b T \mu. \tag{12}$$

Thus, the diffusive properties of the particle are completely determined by its hydrodynamic mobility.

For an axisymmetric particle, the friction (and mobility) tensors have a high degree of symmetry. In a bulk system, the configuration of a particle is given by its axial unit vector $u$, and the friction tensor can be explicitly written as

$$\zeta^u = \zeta^u_{uu} + \zeta^u_{u1}(1 - uu), \tag{13}$$

$$\zeta^r = \zeta^r_{uu} + \zeta^r_{u1}(1 - uu), \tag{14}$$

$$\zeta^{ur} = \zeta^{ru} = 0, \tag{15}$$

using only four coefficients. For ellipsoids, analytical formulae are available for the bulk diffusion tensor and are listed in appendix A. Otherwise, efficient schemes for the calculation of bulk hydrodynamics properties of macromolecules modelled as collections of beads, such as Hydro++ [25, 26], GRPY [27], or Hydromultipole [24, 28] are also available.

The presence of a confining boundary changes this situation, since the hydrodynamic tensors now depend both on the distance to the boundary, and on the orientation of the nano-rod with respect to the surface. The friction tensors of a near-wall particle, $\zeta_w$, may be written as:

$$\zeta_w = \zeta_0 + \Delta \zeta_w, \tag{16}$$

where $\zeta_0$ is the bulk resistance tensor, and the last term is a wall-induced correction. An analytical leading-order approximation to $\Delta \zeta_w$ with the expansion parameter $L/H$ being the ratio of the size of the particle, $L$, to the wall–particle distance $H$, was derived previously by some of us [29]. Earlier works provide the components of the diffusion tensor for very slender filaments close to walls only for particular alignments [30, 31]. The treatment proposed in reference [29] allows for an efficient calculation of the diffusion tensor of a slender rod-like particle for moderate and large wall–particle distances. By inverting $\zeta_w$ from equation (16), we arrive at a convenient approximation to the near-wall mobility $\mu_w = \zeta_w^{-1}$, which will serve as the starting point for present work. The correction terms have the following form

$$\Delta \zeta_{uu}^w = -\frac{A_1}{2H} + \frac{A_2}{(2H)^2} + O(H^{-3}), \tag{17}$$

$$\Delta \zeta_{rr}^w = -\frac{B}{(2H)^2} + O(H^{-3}), \tag{18}$$

$$\Delta \zeta_{ur}^w = -\frac{C}{(2H)^3} + O(H^{-4}). \tag{19}$$

The tensors $A_{1,2}$, $B$, $C$ above are derived from the multipole expansion of the Blake tensor [32] (Green’s function for the wall-bounded geometry) and they depend on the bulk components of the friction tensor of a rod-like particle and its orientation angle $\theta$ but not on the wall–particle distance. For completeness, we write them explicitly in appendix B.

Notably, there are other strategies for tackling the problem of near-wall mobility or various levels of accuracy, such as boundary integral equations [33] or finite element method simulations [34]. Approximate bead-model numerical schemes on a similar level of accuracy to the analytical correction above supplemented by lubrication treatment of close configurations have been introduced by Swan and Brady [35]. More accurate multipole expansion approaches have also been developed [36]. However, comparisons of the analytical correction presented above in equations (17–20) with accurate bead-model HYDROMULTIPOLE scheme [36] for a rod of aspect ratio $\rho = 10$ have shown the validity of the correction for distances up to $H/L \sim 1$, provided that the rod is far from touching the wall, in which case lubrication corrections become important. Thus, in this contribution we will use the approximate correction, bearing in mind that the analysed model has been developed for moderate particle-nanopore distances. Here, we restrict our attention to the semi-analytical scheme presented above, since the dynamics occur mostly in the range of wide separations of the particle and the wall.

3. Results

3.1. Scaling analysis

The length of the particle is $L$. For dsDNA the length of $L = 100$ bp corresponds to ca 34 nm. Another length scale in the problem is the electrostatic capture radius $\lambda_e$, which at room temperature is in the range of micrometers [15], so $\lambda_e/L \gg 1$.

The interplay between different time scales in the problem determines the ranges in which different mechanisms of capture dominate. We list them all for convenience in table 1. Far enough from the pore, the dynamics are purely Brownian, and the relevant time scale is $\tau_B \sim L^2/(D') \approx 6\pi \eta L^3/k_B T$, where $(D')$ is the average diffusion coefficient of the nano-rod. Rotational Brownian motion occurs on the same time scale $1/(D') \sim 8\pi \eta L^3/k_B T$. In the presence of an electrostatic force (7) driving the translational motion, the velocity scales as $V$ ~
In this case, the anisotropic particle subject to a central force without the wall influence and with no external torque. By comparing the Brownian and electrostatic rotational time scale, we recover the scaling for the orientational capture radius defined in reference [15]. We note that in the mobility (or diffusion) matrix $\mu$, the translational elements scale as $\eta L$, the coupling terms as $\eta L^2$, and the rotational terms as $\eta L^3$. This scaling changes close to the wall, where an additional length scale, the wall–particle distance $H$, comes into play. When the rod comes close to the wall, reorientation due to hydrodynamic interactions with the boundary becomes important, with the relevant time scale $\tau_w$ derived from the scaling form of the equation $\Omega = \mu^\epsilon \cdot F_e + \mu^\perp \cdot T_e$. By comparing different time scales we determine four general regimes of motion, sketched in figure 2. The furthest region is Brownian, but closer to the pore when $\tau_B \sim \tau_e$, translational motion is driven by electrostatic forces but rotational motion remains Brownian. Moving even closer, electrostatic torque dominates over thermal reorientation. The boundaries between these regions are determined by the radial distance from the pore. However, in the vicinity of the wall, the diffusivity and hence mobility are generally hindered by hydrodynamic interactions with the wall, which become the dominant driving mechanism. We thus conclude that for the analysis of the behaviour of a field-driven nanorod, since we focus on the dynamics in the range $L < r \ll \lambda_e$, Brownian motion may be neglected, as it would only influence the initial orientations with which the rod would enter the area dominated by electrostatic interactions. It is essential, however, to retain the hydrodynamic anisotropy of the rod, as it influences both the translational and rotational motion in the presence of a strong electric field.

For quantitative calculations, we choose dimensionless units with the basic length $L$. In the presence of an electric field, the more appropriate time unit is $\tau = \tau_B L/\lambda_e = 6\pi\eta L^2/k_B T \lambda_e$. For dsDNA mentioned above, this time scale is of the order of $10^{-7}$ s. With this choice, we can write the force and torque acting on the rod as

$$F_e = \frac{\dot{r}}{r^2}, \quad T_e = -\frac{(\dot{r} \cdot u)(\dot{r} \times u)}{r^3}. \quad (21)$$

### Table 1. Time scales in the system.

| Symbol | Scaling | Description |
|--------|---------|-------------|
| $\tau$ | $6\pi\eta L^2/k_B T \lambda_e$ | Basic time scale |
| $\tau_B$ | $6\pi\eta L^3/k_B T$ | Brownian (diffusive) time |
| $\tau_e^\perp$ | $6\pi\eta L^2 r^2/k_B T \lambda_e$ | Electrostatic translation time |
| $\tau_e^\parallel$ | $6\pi\eta L^3/k_B T \lambda_e$ | Electrostatic rotation time |
| $\tau_w$ | $6\pi\eta H^2 r^2/k_B T \lambda_e$ | Wall-induced rotation time |

$(D^4 \lambda_e r^2 \sim k_B T \lambda_e/6\pi\eta L^2)$. Thus the relevant translational time scale is $\tau_e^\perp \sim L/V = 6\pi\eta L^2 r^2/k_B T \lambda_e$. The electrostatic torque falls off quicker with distance, so the relevant rotation time scale derived from it becomes $\tau_e^\parallel \approx 6\pi\eta L^3 r^3/k_B T \lambda_e$. By comparing the Brownian and electrostatic rotational time scale, we recover the scaling for the orientational capture radius defined in reference [15]. We note that in the mobility (or diffusion) matrix $\mu$, the translational elements scale as $\eta L$, the coupling terms as $\eta L^2$, and the rotational terms as $\eta L^3$. This scaling changes close to the wall, where an additional length scale, the wall–particle distance $H$, comes into play. When the rod comes close to the wall, reorientation due to hydrodynamic interactions with the boundary becomes important, with the relevant time scale $\tau_w$ derived from the scaling form of the equation $\Omega = \mu^\epsilon \cdot F_e + \mu^\perp \cdot T_e$. By comparing different time scales we determine four general regimes of motion, sketched in figure 2. The furthest region is Brownian, but closer to the pore when $\tau_B \sim \tau_e$, translational motion is driven by electrostatic forces but rotational motion remains Brownian. Moving even closer, electrostatic torque dominates over thermal reorientation. The boundaries between these regions are determined by the radial distance from the pore. However, in the vicinity of the wall, the diffusivity and hence mobility are generally hindered by hydrodynamic interactions with the wall, which become the dominant driving mechanism. We thus conclude that for the analysis of the behaviour of a field-driven nanorod, since we focus on the dynamics in the range $L < r \ll \lambda_e$, Brownian motion may be neglected, as it would only influence the initial orientations with which the rod would enter the area dominated by electrostatic interactions. It is essential, however, to retain the hydrodynamic anisotropy of the rod, as it influences both the translational and rotational motion in the presence of a strong electric field.

For quantitative calculations, we choose dimensionless units with the basic length $L$. In the presence of an electric field, the more appropriate time unit is $\tau = \tau_B L/\lambda_e = 6\pi\eta L^2/k_B T \lambda_e$. For dsDNA mentioned above, this time scale is of the order of $10^{-7}$ s. With this choice, we can write the force and torque acting on the rod as

$$F_e = \frac{\dot{r}}{r^2}, \quad T_e = -\frac{(\dot{r} \cdot u)(\dot{r} \times u)}{r^3}. \quad (21)$$

### 3.2. Discussion of trajectories

Before focussing on the numerical solutions of the full set of equations, it is informative to consider a very simple case of an anisotropic particle subject to a central force without the wall influence and with no external torque. In this case, the particle’s mobility tensor has the form as in equation (13), with two coefficients $\mu_{\parallel}, \mu_{\perp}$. For very slender rods, we have $\mu_{\parallel} \approx 2\mu_{\perp}$.

We can describe such a situation by taking a coordinate system centred at the pore, and oriented with the principal axes of the body (||, ⊥). Within this parametrisation, the equations of motion of the centre of the rod $(r_{1, r})$ are

$$\frac{\partial r_{\parallel}}{\partial t} = \frac{\mu_{\parallel}}{r} F(r) r_{\parallel}, \quad \frac{\partial r_{\perp}}{\partial t} = \frac{\mu_{\perp}}{r} F(r) r_{\perp}. \quad (23)$$

By displaying the equations in this form, it is immediately clear that the function $F(r)$ only influences the time dependence and has no bearing on the trajectory. For bounded $F$, there is a hyperbolic fixed point at the origin with two important trajectories intersecting at it: $r_{\parallel} = 0$ and $r_{\perp} = 0$. The first corresponds to slower, sideways motion and the second to faster, axial motion. We conclude that a particle with different values of the drag coefficients along different axes will almost always approach the fixed point along the slowest axis, which in the case of a rod-like colloids means that the particles would most often approach the pore broadside. This conclusion holds sway whenever the torques acting on the rod are negligible and thus it concisely describes the initial dynamics when starting far enough from the pore. Approaching the slow rectilinear trajectory is accomplished by hydrodynamic ‘gliding’ effect where velocity stays at an angle to the force in the initial stages of motion. Moreover, we predict the existence of two types of trajectories—concave and convex—depending on whether rod initially points towards or away from the wall compared to the pore direction.
To explore the dynamics driven by the interplay between electrostatic and hydrodynamic forces acting on the nanorod, we integrate the deterministic equations of motion numerically. As argued before, we neglect the influence of Brownian motion in the range of distances under consideration. The equations of motion for the system are
\[
(V \Omega) = \frac{\mu_w}{w} \left( F_e T_e \right),
\]
which together with equations (3) and (4) allow us to calculate the trajectories of nano-rods. We consider an ellipsoidal rod of aspect ratio \( p = 10 \). We integrated the equations of motion using NDSolve command of Mathematica 12.1 with Method -> {“EquationSimplification” -> “Residual”} option enabled to deal with algebraic-differential nature of the equations.

We present the resulting trajectories in figure 3, starting from a point \( r_0 = (35, 25) \) above the wall, thus seen at an angle \( \alpha_0 \approx 2\pi/9 \) from the nanopore. Rods starting at different orientations glide sideways with respect to the field direction due to their shape (and therefore also mobility) anisotropy. For the initial angle \( \theta_0 < \alpha_0 \), the trajectories are convex and they approach the vicinity of the pore from below the direction \( \alpha_0 = \theta_0 \). The initial inclination \( \theta_0 > \alpha_0 \) leads to a concave path gliding above the \( r_0 \) direction. The shape of the trajectories is also dependent on the aspect ratio of the nanorod, which determines the parallel and perpendicular friction (mobility) coefficients. At large distances, the wall does not influence the observed dynamics. A closer look into the particles’ orientations, sketched in figure 4 for four chosen initial orientations \( (\theta_0 = k\pi/36, \text{with} \ k = 3, 11, 22, 34) \), reveals a strong alignment with the field lines, predicted by earlier works neglecting hydrodynamic anisotropy [15]. The time dependence of the rods’ orientation shows a systematic change, the rate of which increases when approaching the pore due to the increasingly strong attractive force and aligning torque. At the considered separations from the pore, we see no pronounced effect of the translation–rotation coupling due to the wall, which in this case is too weak to compete with field-driven motion. It would come into significance at near-touching configurations where we also expect the detailed geometry of the pore to matter.

To test how strong the alignment with the field lines is, in figure 5 we present the results of numerical simulations for a spectrum of initial orientation angles \( \theta_0 \) for rods released far away from the pore at three representative values of the polar angle \( \alpha_0 \). For each starting configuration, we determine the final orientation \( \theta_f \) and plot the final angle to the local field line, \( |\alpha_f - \theta_f| \), at the final position of the particle. For most initial values of the approach angle, conclusions are similar to those from models neglecting wall interaction terms—the final deviation angle from the field lines direction is typically of the order of \( \pi/50 \). For small angles \( \alpha_0 \), however, the relationship
regimes of motion. The nanopore is modelled as a point charge driven by the electric field of a nanopore in a viscous fluid with a particular focus on the inclusion of hydrodynamic interactions and a detailed analysis of the different regimes of motion. The nanopore is modelled as a point charge which attracts a uniformly charged rod-like particle. Basing on scaling arguments, we identified the various time scales of motion and demonstrated that far away from the pore the motion of the particle is purely Brownian but as soon as it reaches the electrostatic capture radius $\lambda_e$ it is systematically attracted towards the pore. Its initial dynamics are then governed by an electrostatic force driving its translational motion, with the velocity resulting from the balance of this force and the fluid drag force. Since the latter is anisotropic, and depends on the orientation of the particle, the motion resembles sideways gliding towards the pore. At closer distances, the electrostatic torque becomes pronounced and strongly aligns the rods with the electric field lines, as reported previously [15]. However, earlier studies neglected the role of hydrodynamic interactions both on the level of the particle anisotropy, and the wall-induced increase of friction.

In this contribution, we have outlined a theoretical approach which takes into account both the anisotropy of the particle and the wall hindrance effect. Supported by scalings, we explored the trajectories at intermediate distances, when Brownian motion can be neglected, but the rod is far enough from the pore to disregard the field and flow effects of the pore geometry. At large and moderate distances, we have employed an approximate analytical scheme, in which the friction tensor of a colloid close to the wall can be decomposed into its bulk value, encoding the particle anisotropy, and a wall-induced correction. This allowed us to formulate a deterministic system of equations which can be solved for arbitrary initial position and orientation of the nano-rod.

For starting points at a large polar angle $\alpha$, we find that gliding trajectories are governed by the shape anisotropy of the rod, and the wall plays no significant role. However, for smaller approach angles, hydrodynamic interactions with the wall significantly alter the angle at which the rod approaches the near-pore region. We have shown the extent of this region to be as large as $\pi/8$ which accounts for nearly 40% of spherical area in 3D, thus signifying the importance of wall effects in the proper modelling of dynamics in confined geometry.

Our work shows, basing on a scaling analysis, that it is justified to neglect the role of Brownian motion in the near-pore region. Previous works on a similar system included Brownian motion on the level of translational motion only, by imposing a constant diffusion coefficient of the particle [15]. However, in order to properly resolve the question of Brownian displacements and rotations, one should account for two facts: (a) the non-spherical shape of the rod which makes its diffusion anisotropic even in a bulk system, and (b) the presence of the wall which renders the anisotropic diffusion tensor of the particle a wall–particle distance-dependent and introduces translation–rotation coupling. Even then, we would expect the effect of Brownian motion to be pronounced outside the near-pore region which is dominated by electrostatic interactions. Including these effects would be an interesting direction of future research.

The analysis of trajectories close to the pore remains a separate issue, since its non-planar geometry has a significant influence on the trajectories, both by changing the structure of the electric field, which can no longer be modelled by a
point charge, and by the different character of hydrodynamic interactions, where the pore opening shapes the lubrication flow and friction landscape for the colloid. For an insight into these dynamics, detailed models of the pore structure should be implemented.

Acknowledgments

We thank Piotr Szymczak for helpful discussions. The work of RW and ML was supported by the National Science Centre of Poland Grant Sonata to ML No. 2018/31/D/ST3/02408.

Appendix A. Bulk friction tensors of an ellipsoid

The elements of the bulk friction tensor for an ellipsoidal colloid are known analytically [23]. For a prolate spheroid with a long axis \(a = L/2\) and a short axis \(c\), corresponding to an eccentricity \(e = \sqrt{a^2 - c^2}/a\), the bulk friction coefficients in \(\zeta_0\) can be written as

\[
\zeta_1 = (6\pi \eta a) \frac{8}{3} e^3 \left[-2e + (1 + e^2) \ell \right]^{-1}, \tag{A.1}
\]

\[
\zeta_2 = (6\pi \eta a) \frac{16}{3} e^3 \left[2e + (3e^2 - 1) \ell \right]^{-1}, \tag{A.2}
\]

\[
\zeta_3 = (8\pi \eta a^3) \frac{4}{3} e^3 (1-e^2) \left[2e - (1 - e^2) \ell \right]^{-1}, \tag{A.3}
\]

\[
\zeta_4 = (8\pi \eta a^3) \frac{4}{3} e^3 (2 - e^2) \left[-2e + (1 + e^2) \ell \right]^{-1}, \tag{A.4}
\]

\[
\zeta^{dr} = (\pi \eta a^3) \frac{16}{3} e^3 \left[-2e + (1 + e^2) \ell \right]^{-1}, \tag{A.5}
\]

\[
\ell = \log \left(\frac{1 + e}{1 - e}\right). \tag{A.6}
\]

The last coefficient, \(\zeta^{dr}\), links the stresslet (symmetric dipole moment) on the spheroid with the rate-of-strain tensor of an external flow.

Appendix B. Wall correction terms

The correction terms are described in detail in reference [29]. It is most convenient to specify the components of the near-wall friction tensor in a body-fixed frame of reference. It is defined by a set of basis vectors \(\{\mathbf{u}, \mathbf{u}_{1,1}, \mathbf{u}_{1,2}\}\), where \(\mathbf{u}\) is the director along the long axis of the nano-rod, \(\mathbf{u}_{1,1} = (\mathbf{e}_\perp \times \mathbf{u})/|\mathbf{e}_\perp \times \mathbf{u}|\) is parallel to the wall and perpendicular to the particle axis, and \(\mathbf{u}_{1,2} = \mathbf{u}_{1,1} \times \mathbf{u}\) completes the orthonormal basis. We can write the tensors in equations (17)–(20) explicitly in the body-fixed frame RW. For convenience, we define the following shorthand notation

\[
s \equiv \sin \theta, \quad c \equiv \cos \theta. \tag{B.1}
\]

For the translational part (17), we find the correction’s angular dependence as

\[
A_1 = -\frac{3}{16\pi \eta} \begin{pmatrix}
\left(\zeta_1^\parallel \right)^2(1 + c^2) & 0 & -\zeta_1^\parallel c \zeta_1^\perp \\
0 & (\zeta_1^\perp)^2 - \zeta_1^\parallel c \zeta_1^\perp & 0 \\
-\zeta_1^\parallel c \zeta_1^\perp & 0 & \left(\zeta_1^\perp \right)^2(1 + s^2)
\end{pmatrix}, \tag{B.2}
\]

\[
A_2 = \frac{9}{256\pi^2 \eta^2} \begin{pmatrix}
A_1 & 0 & A_{1,1} \\
0 & A_{1,1} & 0 \\
A_{1,1} & 0 & A_{1,2}
\end{pmatrix}. \tag{B.3}
\]

with the coefficients

\[
A_{1,1} = (\zeta_1^\parallel)^3, \tag{B.4}
\]

\[
A_{1,2} = (\zeta_1^\parallel)^3(1 + c^2) + (\zeta_1^\parallel)^2 \zeta_1^\perp s c, \tag{B.5}
\]

\[
A_{1,1,1} = (\zeta_1^\parallel)^3(1 + s^2) + (\zeta_1^\parallel)^2 \zeta_1^\perp s c, \tag{B.6}
\]

\[
A_{1,1,2} = -\zeta_1^\parallel [\zeta_1^\parallel (1 + c^2) + \zeta_1^\perp (1 + s^2)] sc. \tag{B.7}
\]

Finally, the rotational part \(C\) in equation (20) has the form

\[
C = -\frac{1}{16\pi \eta} \begin{pmatrix}
(\zeta_1^\parallel)^2(5 - 3c^2) & 0 & -3\zeta_1^\parallel \zeta_1^\perp sc \\
0 & 5(\zeta_1^\perp)^2 - sc & 0 \\
0 & 0 & (\zeta_1^\perp)^2(5 - 3s^2)
\end{pmatrix} + \frac{3\zeta_1^\parallel}{16\pi \eta} \begin{pmatrix}
0 & 0 & -2\zeta_1^\parallel (1 - 2c^2) \zeta_1^\perp sc \\
0 & 0 & 2\zeta_1^\parallel \zeta_1^\perp sc \\
0 & 3 + c^2 - 4c^2 & 0
\end{pmatrix} - \frac{3(c^{dr})^2}{16\pi \eta} \begin{pmatrix}
0 & 0 & 0 \\
0 & 0 & 0 \\
0 & 0 & 1 + 2c^2
\end{pmatrix}. \tag{B.9}
\]

ORCID iDs

Radost Waszkiewicz  
https://orcid.org/0000-0002-0376-1708

Maciej Lisicki  
https://orcid.org/0000-0002-6976-0281

References

[1] Wanunu M 2012 Nanopores: a journey towards DNA sequencing  Phys. Life Rev. 9 125–58
[2] Branton D et al 2008 The potential and challenges of nanopore sequencing  Nat. Biotechnol. 26 1146–53
[3] Henriksson S E, Misakian M, Robertson B and Kasianowicz J J 2000 Driven DNA transport into an asymmetric nanometer-scale pore  Phys. Rev. Lett. 85 3057–60
[4] Kasianowicz J J, Brandin E, Branton D and Deamer D W 1996 Characterization of individual polynucleotide molecules using a membrane channel  Proc. Natl Acad. Sci. 93 13770–3
[5] Pradeep W, Hu R, Prasad B, Yamazaki H, Cressiot B, Zhao Q, Whitford P C and Wanunu M 2017 Nanopore-based measurements of protein size, fluctuations, and conformational changes ACS Nano 11 5706–16
[6] Amit M, Nivon L and Branton D 2001 Voltage-driven DNA translocations through a nanopore Phys. Rev. Lett. 86 3435–8
[7] Forrey C and Muthukumar M 2007 Langevin dynamics simulations of ds-DNA translocation through synthetic nanopores J. Chem. Phys. 127 015102
[8] Ye A and Qian S 2011 Electrokinetic particle translocation through a nanopore Phys. Chem. Chem. Phys. 13 4060–71
[9] Muthukumar M 2010 Theory of capture rate in polymer translocation J. Chem. Phys. 132 195101
[10] Hatlo M M, Panja D and van Roij R 2011 Translocation of DNA molecules through nanopores with salt gradients: the role of osmotic flow Phys. Rev. Lett. 107 068101
[11] Jeon B J and Muthukumar M 2014 Polymer capture by α-hemolysin pore upon salt concentration gradient J. Chem. Phys. 140 015101
[12] Szymczak P 2014 Translocation of knotted proteins through a pore Eur. Phys. J. Spec. Top. 223 1805–12
[13] Grosberg A Y and Rabin Y 2010 DNA capture into an nanopore: J. Phys.: Condens. Matter
[14] Qiao L, Ignacio M and Slater G W 2019 Voltage-driven translocation of rod-like molecules by a nanopore: defining an ‘orientational capture radius’ J. Chem. Phys. 152 144902
[15] Qiao L and Slater G W 2020 Capture of rod-like molecules by a nanopore: defining an ‘orientational capture radius’ J. Chem. Phys. 152 144902
[16] Russel W B, Hinch E J, Leal L G and Tiefenbruck G 1977 Rods falling near a vertical wall J. Fluid Mech. 83 273
[17] Mitchell W H and Spagnolie S E 2015 Sedimentation of spheroidal bodies near walls in viscous fluids: glancing, reversing, tumbling and sliding J. Fluid Mech. 772 600–29
[18] Happel J and Brenner H 1991 Low Reynolds Numbers Hydrodynamics (Dordrecht: Kluwer)
[19] Dogic Z and Fraden S 2001 Development of model colloidal liquid crystals and the kinetics of the isotropic–smectic transition Phil. Trans. R. Soc. A 359 997–1015
[20] McMullen A, de Haan H W, Tang J X and Stein D 2014 Stiff filamentous virus translocations through solid-state nanopores Nat. Commun. 5 4171
[21] de Haan H W and Slater G W 2013 Translocation of ‘rod-coil’ polymers: probing the structure of single molecules within nanopores Phys. Rev. Lett. 110 048101
[22] Sharma R K, Agrawal I, Liang D, Doyle P S and Garaj S 2019 Complex DNA knots detected with a nanopore sensor Nat. Commun. 10 4473
[23] Kim S and Karrila S J 1991 Microhydrodynamics: Principles and Selected Applications (Boston: Butterworth-Heinemann)
[24] Ekiel-Jezewska M L and Wajnryb E 2009 Precise multipole method for calculating hydrodynamic interactions between spherical particles in the Stokes flow Theoretical Methods for Micro Scale Viscous Flows ed F Feuillebois and A Sellier (Kerala: TransWorld Research) pp 127–72
[25] Garcia de la Torre J, del Rio Echenique G and Ortega A 2007 Improved calculation of rotational diffusion and intrinsic viscosity of bead models for macromolecules and nanoparticles J. Phys. Chem. B 111 955–61
[26] Fernandes M X and Garcia de la Torre J 2002 Brownian dynamics simulation of rigid particles of arbitrary shape in external fields Biophys. J. 83 3039–48
[27] Zuk P J, Cichocki B and Szymczak P 2018 GRPY: an accurate bead method for calculation of hydrodynamic properties of rigid biomacromolecules Biophys. J. 115 782–800
[28] Cichocki B, Felderhof B U, Hinsen K, Wajnryb E and Bławzdziewicz J 1994 Friction and mobility of many spheres in Stokes flow J. Chem. Phys. 100 3780–90
[29] Lisicki M, Cichocki B and Wajnryb E 2016 Near-wall diffusion tensor of an axisymmetric colloidal particle J. Chem. Phys. 145 034904
[30] Katz D P, Blake J R and Paveri-Fontana S L 1975 On the movement of slender bodies near plane boundaries at low Reynolds number J. Fluid Mech. 72 529–40
[31] De Mestre N J and Russel W B 1975 Low-Reynolds-number translation of a slender cylinder near a plane wall J. Eng. Math. 9 81–91
[32] Blake J R 1971 A note on the image system for a Stokeslet in a no-slip boundary Math. Proc. Camb. Phil. Soc. 70 303–10
[33] Hsu R and Ganatos P 1989 The motion of a rigid body in viscous fluid bounded by a plane wall J. Fluid Mech. 207 29–72
[34] De Corato M, Greco F, D’Avino G and Maffettone P L 2015 Hydrodynamics and Brownian motions of a spheroid near a rigid wall J. Chem. Phys. 142 194901
[35] Swan J W and Brady J F 2007 Simulation of hydrodynamically interacting particles near a no-slip boundary Phys. Fluids 19 113306
[36] Cichocki B, Jones R B, Kutteh R and Wajnryb E 2000 Friction and mobility for colloidal spheres in Stokes flow near a boundary: the multipole method and applications J. Chem. Phys. 112 2548