Influence of glenoid wear pattern on glenoid component placement accuracy in shoulder arthroplasty

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Background: Accurate glenoid component placement in shoulder arthroplasty is often difficult even with the use of preoperative planning. Computer navigation and patient-specific guides increase component placement accuracy, but which patients benefit most is unknown. Our purpose was to assess surgeons’ accuracy in placing a glenoid component in vivo using 3-dimensional preoperative planning and standard instruments among various glenoid wear patterns.

Methods: We conducted a retrospective review of 170 primary anatomic total shoulder arthroplasty (aTSA) and reverse total shoulder arthroplasty (rTSA) performed at a single institution. Commercially available preoperative planning software was used in all arthroplasties with multiplanar 2-dimensional computed tomography and a 3-dimensional implant overlay. After registration of intraoperative bony landmarks to the navigation system, participating surgeons with knowledge of the preoperative plan were blinded to the computer screen and attempted to implement their preoperative plan by simulating placement of a central-axis glenoid guide pin. Two hundred thirty-three screenshots of surgeon’s simulated guide pin placement were included. Glenoid displacement, error in version and inclination, and overall malposition from the preoperatively planned target point were stratified by posterior wear status (with [Walch B2 or B3] or without [A1, A2, or B1]) and Walch classification (A1, A2, B1, B2, or B3).

The glenoid component was considered malpositioned when version or inclination errors exceeded 10\degree or the starting point displacement exceeded 4 mm.

Results: For rTSA, errors in version were greater for glenoids with posterior wear compared with those without (8.1\pm 5.6 vs. 4.7\pm 4.0; P < .001). On post hoc analysis, B2 glenoids had greater version error than A1, A2, and B1 glenoids. A greater proportion of glenoids undergoing rTSA that possessed posterior wear had an error in version \textgreater 10\degree compared with those without (31\% vs. 8\%; P < .001). Consequently, glenoids undergoing rTSA with posterior wear were malpositioned at a greater rate compared with those without (73\% vs. 53\%). In contrast, glenoids undergoing aTSA with and without posterior wear did not differ based on displacement error, version error, inclination error, or malposition occurrence.

Conclusions: Posterior glenoid bone loss more commonly resulted in glenoid version errors exceeding 10 degrees and component malposition in rTSA, but not for aTSA. Malposition was still relatively high in patients without significant posterior wear for both aTSA (36\%) and rTSA (53\%). Surgeons should consider alternate techniques beyond preoperative planning and standard instrumentation when performing shoulder arthroplasty in patients with posteriorly worn glenoids.

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Implant positioning is critical to successful total shoulder arthroplasty and remains a significant, surgeon-modifiable risk factor for decreased implant longevity. In anatomic total shoulder arthroplasty (aTSA), placement of the glenoid implant in neutral version leads to less chance of osteolysis and glenoid loosening.\textsuperscript{11}
Conversely, retroverted glenoid implants (ie, those with retroversion > 10°) have been associated with increased rates of component loosening.\(^3,12,15,23\) Similarly, accurate glenoid placement in reverse total shoulder arthroplasty (rTSA) is important to prevent scapular notching, which is associated with poorer patient outcomes.\(^5,18,22,26\)

Commercially available preoperative planning software has become widely adopted with the goal of improved glenoid implant placement in both aTSA and rTSA. Preoperative planning has improved glenoid implant placement even when standard instrumentation is used.\(^9,14,16,25,36\) However, precise placement of glenoid implants in vivo remains difficult because of the limited visualization of anatomic landmarks of the scapula during shoulder arthroplasty.\(^32\) To better replicate preoperative plans, 2 primary methods have gained popularity: computer navigation and patient-specific instrumentation. Both of these technologies have demonstrated improved accuracy of glenoid placement.\(^3,7,10,30,35\) However, increased cost, low availability, and lack of proven clinical benefit to patients have remained impediments to uniform adoption. Identifying patient risk factors for implant malposition could enable more selective use of computer navigation and patient-specific instrumentation, thereby benefiting patients at greater risk for implant malposition without burdening patients that would not see significant benefit of additional costs.

In this study, we sought to determine if surgeons’ ability to accurately execute their preoperative plan varied based on the native glenoid morphology. We hypothesized that glenoids with posterior wear would be associated with greater malposition of glenoid implants when only 3-dimensional preoperative planning was used in vivo during shoulder arthroplasty.

**Methods**

A retrospective review of all primary shoulder arthroplasties performed between September 2017 and March 2020 was performed from a single institution. In 2017, 3-dimensional preoperative planning software and intraoperative computer navigation (Equinoxe Planning App and Exactech GPS; Exactech, Gainesville, FL, USA) were introduced to our practice; subsequently, nearly all primary shoulder arthroplasties, both aTSA and rTSA, performed at our institution used this technology both pre- and intraoperatively. After the introduction of this technology, 4 fellowship-trained shoulder arthroplasty surgeons began to measure and track their individual accuracy at placing the glenoid implant based on their preoperative plan. Procedures for which navigation was unable to be performed or screenshots were not available for analysis were excluded from this study.

**Preoperative planning**

Preoperatively, participating surgeons reviewed 2D and 3D computed tomography (CT) scan reconstructions using the preoperative planning software. The software provides 2D multplanar CT imaging with 3D implant overlay. Participating surgeons (always at least one attending, fellowship-trained shoulder surgeon, sometimes with one or more upper extremity fellows) collaborated to use the planning software to determine appropriate implant placement based on patient-specific glenoid morphology. In all cases, the final decision on implant placement was made by the attending surgeon. In some cases, full-wedge augments were planned for both in aTSA and rTSA based on surgeon discretion. The planned case was then saved and uploaded to the operating room computer navigation unit for use during surgery.

**Operative technique**

All surgical procedures were performed through a deltopectoral approach. The incision was extended proximally approximately 1–2 cm past the coracoid tip to enable complete and adequate exposure for the placement of the coracoid tracker used for computer navigation. Management of the subscapularis was per surgeon preference, with either lesser tuberosity osteotomy or subscapularis peel for aTSA and subscapularis peel or tenotomy for rTSA. The humerus was exposed with extension and external rotation after an inferior capsular release. For aTSA, the head was cut in its native retroversion. For rTSA, the head underwent osteotomy in either 20° of retroversion or its native retroversion, per surgeon preference, using an extramedullary guide. The glenoid was then exposed in a routine fashion. The biceps if present was routinely tenodesed to the pectoralis major tendon, and the remaining proximal stump and labral tissue were removed. Any remaining cartilage was carefully removed using a Cobb elevator. Soft tissue was released off of the anterior glenoid neck. The base of the coracoid was exposed using electrocautery. The coracoacromial ligament was preserved, and the superior aspect of the coracoid was exposed. The tracker stand was then secured in place with 2 screws (eg, see Fig. 1). The glenoid bony surface was registered according to the manufacturer’s protocol to link the patient’s CT scan and preoperative plan to the visualized anatomy.

**Study protocol**

At this point, all surgeons were blinded from viewing the navigation screen. Using standard instruments and visible anatomic landmarks, and with knowledge of the preoperative plan, surgeons attempted to identify the planned starting point for the central cage of the implant, similar to the placement of the central-axis pin used by many shoulder arthroplasty systems. Participating surgeons then aligned the guided drill in their perceived planned axis (version and inclination), and a screenshot was taken for
retrospective comparison to the preoperative plan (eg, see Fig. 2). Participating surgeons were blinded from the images taken and other surgeons’ positioning. Subsequently, participating surgeons were unblinded to the navigation screen and continued the procedure using computer navigation according to the preoperative plan (eg, see Fig. 1).

Data analysis

Eligible patients were identified, and screenshots were collected and blinded for analysis. An independent evaluator reviewed all screenshots and recorded the displacement from the planned starting point, the magnitude of version error, and the magnitude of inclination error. All values were determined based on the starting central-axis guide pin. Displacement between the preoperative (planned) starting point and the simulated starting point identified intraoperatively by blinded participating surgeons was measured on the screenshots using a validated computer screen measurement program (eg, see Fig. 3; ImageJ; National Institutes of Health, Washington, DC, USA). Intraoperative version and inclination were measured directly by the navigation system and compared with preoperative (planned) version and inclination. Differences in the preoperatively planned measurements and blinded intraoperative positioning from each participating surgeon were computed. Intraoperative blinded execution was considered malpositioned based on previously published criteria: version or inclination errors exceeding 10° or starting point displacement exceeding 4 mm.31 Glenoid morphology was classified based on the Walch classification.2,34 Measurements were stratified by posterior wear status (with, Walch type B2 or B3; without, Walch type A1, B1, or A2) and specific Walch classification (A1, A2, B1, B2, or B3) and were compared based on error from the preoperative plan in displacement, version, and inclination. Only one glenoid was classified as Walch type C in our cohort and was excluded because of lack of statistical power.

Statistical analysis

Displacement, version error, and inclination error on a continuous scale were compared between glenoids with and without posterior wear using an unpaired 2-sided t-test. In addition, differences based on specific Walch classification (A1, A2, B1, B2, or B3) were compared using a one-way analysis of variance test. Version and inclination error were also grouped categorically (<5°, between 5° and 10°, and >10°) and compared based on posterior wear status and specific Walch classification using chi-square tests. Significant interactions were followed by a Tukey (continuous data) or Bonferroni (categorical data) post hoc test for pairwise comparisons where appropriate. All statistics were performed separately for aTSA and rTSA using R Software (version 3.6.3, R Core Team, Vienna, Austria), and the significance was set at a P-value of 0.05.

Results

From our institutional database, we initially identified 368 primary aTSA and rTSA performed during the study period. From these, 233 images from 170 shoulder arthroplasties were included. The mean age at surgery was 69.2 ± 9.2 years, and 53% were female.
Seventy percent of images were from rTSA cases. Glenoids were classified as posteriorly worn (Walch type B2 or B3) in 90 images and not posteriorly worn (A1, A2, or B1) in 143 images. Specifically, the Walch classification of included images are as follows: type A1 in 63 (27%), type A2 in 32 (14%), type B1 in 48 (21%), type B2 in 84 (36%), and type B3 in 6 (3%).

Displacement error

The mean displacement from the planned starting point was $3.5 \pm 2.8$ mm, with 68 measurements (29%) exceeding 4 mm. Displacement error did not differ between glenoids with and without posterior wear for aTSA ($2.7 \pm 2.7$ mm vs. $3.0 \pm 2.0$ mm; $P = .560$) nor rTSA ($4.0 \pm 3.8$ mm vs. $3.7 \pm 2.3$ mm; $P = .518$; Table I). Similarly, glenoids with and without posterior wear were displaced from the starting point by over 4 mm at similar rates for aTSA ($21\% [8]$ vs. $16\% [5]$; $P = .874$) and rTSA ($35\% [18]$ vs. $33\% [37]$; $P = .917$).

Version error

The mean magnitude of version error was $5.7^\circ \pm 4.7^\circ$ (range, 0° to 21°). Forty-four percent of cases deviated more than 5° from the preoperative plan, and 16% deviated beyond 10°. The mean error in version was significantly greater for glenoids with posterior wear than those without for rTSA ($8.1^\circ \pm 5.6^\circ$ vs. $4.7^\circ \pm 4.0^\circ$; $P < .001$), but not aTSA ($5.7^\circ \pm 3.8^\circ$ vs. $5.8^\circ \pm 5.0^\circ$; $P = .875$; Table I). On post hoc pairwise comparison, the magnitude of version error in rTSA was significantly greater for B2 glenoids compared with A1, A2, and B1 glenoids ($P = .002$, $P < .001$, and $P = .015$, respectively; Table II). When classifying version error in 5° increments, glenoids

![Figure 3](image-url) Example of the displacement between the preoperative (planned) starting point and the simulated starting point identified intraoperatively by a blinded surgeon being measured on a computer navigation screenshot using ImageJ.

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**Table I**

| Walch classification | With posterior wear (B2 or B3) (N = 90) | Without posterior wear (A1, A2, or B1) (N = 143) | $P$ value |
|----------------------|----------------------------------------|---------------------------------------------|-----------|
| aTSA, N              | 39                                     | 31                                          | .560      |
| Displacement, mm     | $2.7 \pm 2.7$                          | $3.0 \pm 2.0$                               | .875      |
| Version error, $^a$  | $4.5 \pm 4.8$                          | $4.0 \pm 4.0$                               | .190      |
| Inclination error, $^a$ | $46\% (7)$                            | $36\% (11)$                                | .821      |
| Malposition, % (N)   | $47\% (18)$                            | $36\% (12)$                                | .518      |
| rTSA, N              | 48                                     | 47                                          | $<.001$   |
| Displacement, mm     | $4.7 \pm 3.8$                          | $4.7 \pm 4.0$                               | .327      |
| Version error, $^a$  | $47\% (18)$                            | $40\% (2)$                                 | .537      |
| Inclination error, $^a$ | $47\% (18)$                            | $36\% (12)$                                | .353      |
| Malposition, % (N)   | $50\% (24)$                            | $54\% (23)$                                | .124      |

$aTSA$, anatomic total shoulder arthroplasty; $rTSA$, reverse total shoulder arthroplasty.

Bold values indicate statistical significance.

$^a$As defined by Throckmorton et al.

**Table II**

| Walch classification | A1 | A2 | B1 | B2 | B3 | $P$ value |
|----------------------|----|----|----|----|----|-----------|
| aTSA, N              | 15 | 11 | 5  | 33 | 6  | .849      |
| Displacement, mm     | $2.8 \pm 1.5$ | $2.9 \pm 2.8$ | $4.0 \pm 1.7$ | $2.7 \pm 2.8$ | $2.7 \pm 1.6$ | .300      |
| Version error, $^a$  | $7.1 \pm 5.8$ | $3.6 \pm 2.6$ | $6.8 \pm 5.8$ | $5.5 \pm 3.9$ | $6.8 \pm 3.6$ | .537      |
| Inclination error, $^a$ | $4.5 \pm 4.8$ | $3.2 \pm 2.6$ | $4.4 \pm 5.0$ | $5.2 \pm 4.7$ | $7.3 \pm 8.0$ | .353      |
| Malposition, % (N)   | $47\% (7)$ | $18\% (2)$ | $40\% (2)$ | $36\% (12)$ | $67\% (4)$ | .124      |
| rTSA, N              | 48 | 21 | 43 | 51 | 0  | $<.001$   |
| Displacement, mm     | $3.8 \pm 2.4$ | $4.7 \pm 3.1$ | $3.0 \pm 1.6$ | $4.0 \pm 3.8$ | NA          | .328      |
| Version error, $^a$  | $4.7 \pm 3.8$ | $3.3 \pm 2.9$ | $5.3 \pm 4.5$ | $8.1 \pm 5.6$ | NA          | $<.001$   |
| Inclination error, $^a$ | $7.4 \pm 6.4$ | $6.5 \pm 4.3$ | $8.7 \pm 5.1$ | $8.7 \pm 5.8$ | NA          | .110      |

$aTSA$, anatomic total shoulder arthroplasty; NA, not applicable; rTSA, reverse total shoulder arthroplasty.

Bold values indicate statistical significance.

$^a$As defined by Throckmorton et al.
undergoing aTSA did not differ based on the degree of wear ($P = .543$) nor the specific Walch classification ($P = .267$; Fig. 4). In contrast, glenoids undergoing rTSA differed based on both degree of wear ($P < .001$) or specific Walch classification ($P < .001$) with increased error seen in glenoids with greater posterior wear (Fig. 5). Notably, a greater proportion of glenoids with posterior wear undergoing rTSA had an error in version $> 10^\circ$ ($31\% [16]$ vs. $8\% [9]; P < .001$). Of the glenoids with $> 10^\circ$ of version error (both aTSA and rTSA), glenoids with posterior wear were more commonly overretroverted intraoperatively compared with the preoperative plan compared with glenoids without posterior wear ($55\%$ vs. $31\%$), although this was not statistically significant ($P = .273$).

**Inclination error**

The mean magnitude of inclination error was $7.1^\circ \pm 5.6^\circ$ (range, $0^\circ$ to $26^\circ$), with $53\%$ of measurements exceeding the $5^\circ$ error cutoff and $24\%$ exceeding the $10^\circ$ cutoff. The magnitude of inclination
error did not differ between glenoids with and without posterior wear for aTSA (5.5° ± 5.3° vs. 4.0° ± 4.1°; P = .190) nor rTSA (8.7° ± 5.8° vs. 7.8° ± 5.6°; P = .327; Table I). When classifying inclination error in 5° increments, glenoids did not differ based on either posterior wear status or specific Walch classification for aTSA (P = .395 and P = .351, respectively) nor rTSA (P = .418 and P = .305, respectively; Figs. 6 and 7, respectively).

Figure 6 Inclination error in aTSAs stratified by (A) posterior wear status and (B) Walch classification grouped by <5°, between 5° and 10°, or >10°.

Figure 7 Inclination error in rTSAs stratified by (A) posterior wear status and (B) Walch classification grouped by <5°, between 5° and 10°, or >10°.

error did not differ between glenoids with and without posterior wear for aTSA (5.5° ± 5.3° vs. 4.0° ± 4.1°; P = .190) nor rTSA (8.7° ± 5.8° vs. 7.8° ± 5.6°; P = .327; Table I). When classifying inclination error in 5° increments, glenoids did not differ based on either posterior wear status or specific Walch classification for aTSA (P = .395 and P = .351, respectively) nor rTSA (P = .418 and P = .305, respectively; Figs. 6 and 7, respectively).

Glenoid malposition

Without intraoperative navigation, 53% of glenoids would have been malpositioned based on the Throckmorton criteria (>4 mm of displacement or >10° error in version or inclination). Glenoids with posterior wear would have had a higher rate of malposition compared with glenoids without posterior wear without the use of
intraoperative navigation for rTSA (73% vs. 53%; \(P = .027\)), but not aTSA (41% vs. 36%; \(P = .821\); Table 1).

**Discussion**

Despite widespread adoption of preoperative planning software and evidence supporting the use of guided instrumentation intraoperatively to improve glenoid component placement accuracy, traditional instrumentation remains the most used method for glenoid placement in shoulder arthroplasty. In the present study, we found that simulated glenoid component placement had greater version error when compared with the preoperative plan for glenoids with posterior wear compared with those without in rTSA, but not aTSA. Without the use of intraoperative navigation, the rate of glenoid malposition would have been greater for glenoids with posterior wear undergoing rTSA, but not aTSA; nonetheless, the rate of malposition in aTSA would have been high (39%).

The ability of the surgeons in the present study to reproduce their preoperative plan is similar to previous studies. Displacement from the planned starting point in our study (3.5 mm) was comparable to previously published data (2.89-3.2 mm).\(^{17,30,31}\) Our overall version error (5.7°), inclination error (7.1°), and malposition rate (53%) were within the range of previously published data (4.8°-8°, 4.2°–7°, and 38%-66%, respectively).\(^{17,30,31}\) Similarly, a comparable proportion of glenoid components in the present study were within 5° as reported previously for version (56% vs. 48-51%) and inclination (47% vs. 22-50%).\(^{14,30}\)

To our knowledge, this is the first study to report on glenoid morphology as a specific risk factor for imprecise glenoid component placement in vivo when preoperative planning is used without intraoperative navigation or patient-specific guides. Our finding that there was greater error in version for glenoids with posterior wear undergoing rTSA has potential clinical significance. Glenoids with eccentric wear preoperatively are associated with a greater than 2-fold increased rate of glenoid component loosening compared with glenoids with concentric wear in aTSA.\(^{13}\) In our study, errors in version were significantly more common with posterior glenoid bone loss, compared with displacement and inclination, which did not appear to be affected by posterior glenoid bone loss. These findings highlight the difficulty for surgeons to accurately use intraoperative landmarks, which are altered with posterior glenoid bone loss and increasing glenoid retroversion. To reduce potential complications such as implant loosening, surgeons should consider using a patient-specific guide or computer navigation in shoulders with posterior glenoid bone loss, particularly when performing rTSA.

Preoperative planning software used with computer navigation or patient-specific guides provides more accurate and reproducible positioning and orientation of the glenoid component in aTSA and rTSA.\(^{7,15,23}\) The results of our study demonstrate that glenoids with posterior wear reduce surgeons’ ability to reproduce their preoperative plan when not using patient-specific guides or navigation during rTSA, but not aTSA. This is in agreement with some prior studies; glenoid morphology has been shown to have no significant influence on the accuracy of patient-specific guides during aTSA.\(^{19}\) In contrast, Jacquet et al found that the use of patient-specific guides in aTSA especially improved the position of the central point when operating on severely retroverted (>10°) glenoids.\(^{17}\) Regardless of glenoid morphology, routine use of computer navigation may improve component positioning; Nashikkar et al found that postoperative alignment of glenoid components for patients undergoing aTSA and rTSA with computer navigation was within 5° of the plan for 82% of cases for version and 76% of cases for inclination.\(^{25}\) The use of computer navigation or patient-specific guides in addition to preoperative planning may substantially improve the surgeons’ accuracy when placing the glenoid component, especially in patients with severe posterior glenoid bone loss undergoing rTSA.

Previous authors have suggested that not all patients may benefit from computer navigation or patient-specific guides. Hendel et al found that glenoid component accuracy was significantly increased in patients undergoing primary aTSA with bone deformity and retroversion in excess of 16° when 3-dimensional preoperative planning software with patient-specific guides was used compared with conventional planning and surgical technique.\(^{9}\) However, no difference in the accuracy of glenoid component placement was seen for patients with <7° of retroversion. In contrast, we report high simulated component malposition rates in glenoids without posterior wear for both aTSA and rTSA (36% and 53%, respectively). Similarly, Schoch et al who showed that glenoid components were malpositioned in more than 38% of cases despite the use of preoperative planning.\(^{10}\) These results suggest that there may be a benefit of computer navigation and patient-specific guides for all patients, regardless of glenoid morphology.

There are several issues to consider when adopting patient-specific guides or computer navigation. Currently, it is unclear whether shoulder arthroplasty patients will benefit clinically from these technologies. Patient-specific guides and computer navigation are not new to orthopaedics, and studies of these technologies in the knee have demonstrated no significant improvement in patient-reported outcomes or implant survival despite more anatomic positioning.\(^{28,32,37}\) However, radiographic failure rates of glenoids remain significantly higher than primary hip and knee arthroplasty, suggesting that these technologies may have a greater role in shoulder arthroplasty.\(^{12,21,24}\) A recent meta-analysis including 247 shoulders from 5 studies found that glenoid version was significantly more accurate according to the preoperative plan when computer navigation was used compared with standard instrumentation.\(^{27}\) Furthermore, a difficult learning curve and increased surgery length may not be an issue for these technologies in shoulder arthroplasty: Wang et al showed surgeons could become proficient using intraoperative computer navigation after 8 cases, and surgical time is comparable to procedures performed using standard instrumentation (77.3 vs. 78.5 minutes).\(^{35}\) Although further work is needed to prove their long-term benefit, patient-specific guides and computer navigation are promising solutions for improving surgeon accuracy, especially in patients with posterior glenoid bone loss.

This study has multiple limitations to consider. First, we included data from both attending surgeons as well as fellow trainees (both hand/upper extremity and shoulder/elbow fellows). This may have contributed to elevated malposition rates and increased version error; prior research has demonstrated a learning curve for both nonnavigated\(^{20}\) and navigated\(^{25}\) shoulder arthroplasty. However, our findings are largely consistent with previously reported malposition rates despite including both fellow trainees and attending surgeons.\(^{17,20,31}\) Furthermore, it further represents generalized practice where shoulder arthroplasties are more commonly performed by nonfellowship trained surgeons. Second, our evaluation of a surgeon’s ability to replicate their preoperative plan was based on their hand position held in space at the time of implant central-axis preparation (as measured by the affixed trackers and line-of-sight camera described in the methods), but not on final implant position. Although postoperative radiographs were obtained, cost, radiation exposure, and deviation from the accepted standard of care precluded our ability to obtain routine postoperative CT scans to evaluate final glenoid implant position more completely. However, prior studies have validated the accuracy of this guided technology, and thus, our findings are expected to appropriately predict final implant position.\(^{25}\) Finally, this study...
did not evaluate subjective or objective clinical outcomes; therefore, we remain unable to fully assess the clinical benefit of intra-operative guidance on either patient-reported outcomes or implant survival.

Conclusion

Surgeons are less accurate at executing their preoperative plan regarding version in glenoids with posterior wear (Walch type B2 or B3) compared with those without (A1, A2, or B1) when performing RSA, but not aTSA. Without the use of intraoperative navigation when performing RSA, the rate of malposition would have been greater in glenoids with posterior wear. Although glenoid component displacement, inclination error, and overall malposition did not differ based on glenoid morphology for aTSA, substantial deviations in the preoperative plan were evident in all glenoid types. When performing shoulder arthroplasty with preoperative planning software but without intraoperative navigation or patient-specific guides, surgeons should take additional care to ensure accuracy of glenoid implant placement, especially with respect to version in patients with posterior glenoid bone loss. Furthermore, to improve accuracy of glenoid component placement, surgeons should consider routine use of computer navigation or patient-specific guides.

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