Assessment of Left Ventricular Myocardial Diseases with Cardiac Computed Tomography

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Rapid advances in cardiac computed tomography (CT) have enabled the characterization of left ventricular (LV) myocardial diseases based on LV anatomical morphology, function, density, and enhancement pattern. Global LV function and regional wall motion can be evaluated using multi-phasic cine CT images. CT myocardial perfusion imaging facilitates the identification of hemodynamically significant coronary artery disease. CT delayed-enhancement imaging is used to detect myocardial scar in myocardial infarction and to measure the extracellular volume fraction in non-ischemic cardiomyopathy. Multi-energy cardiac CT allows the mapping of iodine distribution in the myocardium. This review summarizes the current techniques of cardiac CT for LV myocardial assessment, highlights the key findings in various myocardial diseases, and presents future applications to complement echocardiography and cardiovascular magnetic resonance.

**Keywords:** Computed tomography; Myocardium; Myocardial perfusion imaging; Delayed enhancement

**INTRODUCTION**

Increased awareness of left ventricular (LV) myocardial disease is attributed to the widespread use of non-invasive imaging modalities (1). Echocardiography is still a cornerstone of LV diagnostic imaging because it can provide a safe and comprehensive assessment of cardiac structure, function, and regional wall motion. However, echocardiography is operator-dependent, with a relatively low reproducibility, and possible impairment due to a poor acoustic window, limited field of vision, and technical artifacts (2). Cardiovascular magnetic resonance (CMR) is considered the current gold standard for LV morphological and functional assessment due to its accurate measurements of the entire volume and mass without echo-window dependency. In addition, it has a unique role in noninvasive tissue characterization using different pulse sequences (3, 4).

In the last decade, rapid technical advances in computed tomography (CT) have led to the emergence of cardiac CT (CCT) as a comprehensive evaluation of anatomy and function including the coronary arteries and cardiac chambers. Although CCT is not recommended as the primary method of choice in cases of suspected LV myocardial diseases, CT enables multiplanar reconstructions in any desired orientation and can evaluate the echo-window limited areas such as the apex, the posterior portion of the interventricular septum, and the anterolateral wall. Therefore, CCT offers a comprehensive insight into the anatomy and function of cardiac chambers (5). Recent studies have demonstrated that CCT may be an attractive imaging tool for the characterization of LV myocardial diseases based on gross morphology, function, and enhancement, as well as the extracellular volume fraction (ECV). Therefore, CCT is considered complementary to echocardiography and CMR (1, 6). In this review, the current techniques and uses of CCT for LV myocardial assessment...
are discussed. The roles of CCT imaging in the diagnosis of LV myocardial diseases have also been highlighted.

**Anatomical Assessment of the Left Ventricle with CCT**

The left ventricle is a conical structure with thick tubular walls tapering to a rounded apex. It comprises an inlet portion containing the mitral valve and its tension apparatus, an apical portion containing fine trabeculations, and an outlet portion leading to the aortic valve. Normally, the LV free wall is thickest at the cardiac base. The ventricular septum is curved, bulging into the right ventricular cavity. It is muscular except for a small portion immediately beneath the aortic valve (the membranous septum). When the left ventricle is viewed in short-axial cuts, the mitral valve is supported by two groups of papillary muscles in the anterolateral and posteromedial positions. The bases of the papillary muscles are continuous with the muscular trabeculations at the middle-to-apical third of the ventricular wall (Fig. 1) (7-9).

The LV wall consists of three distinct layers: an inner endocardium, a middle myocardium, and an outer epicardium. The myocardium consists primarily of contractile cardiac myocytes, fibroblasts, and an abundant extracellular matrix. The left ventricle is subdivided into three main segments: the apical, middle, and basal portions. This standardized and widely used segmentation of the left ventricle into 17 myocardial segments was introduced by the American Heart Association (10). The different anatomic landmarks partially reflect the distribution of perfusion of the myocardium by the coronary arteries.

**Technical Aspects of CCT**

There are two methods to obtain CCT images according to electrocardiography (ECG)-gating techniques. In prospective ECG-triggered sequential scanning in a “step-and-shoot” technique, the CT images are acquired in a user-selected phase of the patient’s cardiac cycle (usually during mid-diastole). This technique does not allow for the evaluation of LV function and wall motion (Fig. 2). With the retrospective ECG-gated spiral scanning based on continuous data acquisition and table movement at low table feed (low spiral pitch) or ECG-gated volumetric acquisition with a static table (256- and 320-detector-row CT scanner), CT images are obtained at multiple phases of the cardiac cycle for the assessment of LV functional parameters including wall thickness, volume, and mass, and identification of LV regional wall motion abnormality (11-13).

LV volumes and function are evaluated using a triphasic injection protocol to opacify all the cardiac chambers without streak artifact in the superior vena cava. The total contrast volume is usually 50–120 mL. An initial contrast media bolus at 5–7 mL/s is followed by either a slower rate of contrast media injection at 2 mL/s or a 50%:50% saline/
contrast media mixture at 5–7 mL/s and a smaller volume saline bolus (14). Routine CCT is typically acquired during the early arterial phase for coronary artery assessment. However, to ensure sufficient myocardial enhancement, the timing of image acquisition is calculated by adding approximately 2–4 seconds to the measured time of peak aortic root enhancement (usually 100–150 Hounsfield units [HU]) (15).

Currently, CT perfusion has evolved into a robust and non-invasive tool for the detection of myocardial ischemia. There are two approaches—static and dynamic—perfusion CT. Static perfusion CT provides a snapshot of the myocardial blood volume or myocardial enhancement at a single time point during the first-pass of contrast material bolus. A true perfusion defect persists throughout multiple phases and it is visualized in both systole and diastole. These data are also used to identify regional LV wall motion abnormality. Static perfusion CT is easily performed on any CCT scanner although it is highly dependent on the timing of the scan. In addition, cardiac motion artifacts due to increased heart rate during adenosine stress have shown a significant percentage of patients in static perfusion CT. On the other hand, the dynamic first-pass perfusion CT reveals myocardial enhancement at multiple time points during first-pass of the contrast material and it facilitates quantitative analysis of myocardial perfusion. The best cut-off myocardial blood flow value distinguishing ischemic from remote myocardium varies from 75 to 103 mL/100 mL/min. However, the drawbacks of dynamic perfusion CT imaging include higher exposure to radiation (than static perfusion CT) and the limited use of CT scanners (256- or 320-detector-row CT scanners and dual-source Somatom Flash and Force CT scanners [Siemens Healthcare, Forchheim, Germany]) (16-18).

Delayed-enhancement CCT shares similar pathophysiological basis with delayed-enhancement CMR and it facilitates the evaluation of LV myocardial viability or scarring with additional administration of contrast medium (slow injection rate of up to 2 mL/s and volume between 50 and 90 mL). A delayed scan is usually performed after a variable period of 5–15 minutes following the initial administration of contrast medium. The amount of contrast medium, injection rate, and the delay time are adjusted on a case-by-case basis to evaluate for delayed myocardial enhancement (19, 20). Decreased tube voltage (100 or 80 kVp) and prospective ECG triggering reduce the radiation exposure and increase the myocardial contrast in delayed-phase CCT even though the image noise is increased. Delayed hyperenhancement is attributed to the slow washout of iodinated contrast media from the region of infarcted myocardium (Fig. 3) (19-21). Mahnken et al. (22) and Gerber et al. (23) showed that delayed-enhancement CCT imaging can be used to quantify infarct size strongly correlated with CMR-based imaging. ECV is a reproducible and novel index for assessment of myocardial fibrosis and it is calculated as a ratio of the change in HU of the myocardium and the LV blood before (pre-contrast CCT) and
after contrast administration (delayed-enhancement CCT), multiplied by (1-hematocrit). This protocol can be added to routine CCT with only a small increase in radiation dose. It can be used to delineate the myocardial interstitium and provides a new diagnostic test for an under-diagnosed and treatable cause of LV hypertrophy (LVH) and heart failure (24, 25). CCT represents a potential approach to the clinical assessment of diffuse myocardial fibrosis, particularly in patients with contraindications to CMR imaging. The drawback of delayed-enhancement CCT is the increased image noise and scan time. The multi-energy CCT can help to reduce the image noise and increase the contrast-to-noise ratio (21).

There are 4 different types of multi-energy scanners available in clinical practice for tissue characterization, as follows. 1) Dual-source technology: two X-ray tubes are operated at different kVp values (for example, 80 and 140 kVp); 2) Rapid kVp switching technology: The X-ray source switches rapidly between low (80 kVp) and high energy (140 kVp) levels at each X-ray projection; 3) Dual spin technology: Using a 320-detector-row CT scanner, the patient is initially scanned at one energy level (135 kVp) and immediately scanned in the same anatomic location using a different energy level (80 kVp); 4) Dual layer or spectral detector technology: CT contains one X-ray source but two layers of detectors with the top layer absorbing low energy photons and the bottom layer absorbing high energy photons. Multi-energy CT allows the mapping of iodine distribution in the myocardium serving as a marker of myocardial perfusion (26-28). Delayed iodine enhancement imaging has the potential to better evaluate myocardial enhancement, which is considered a marker of myocardial fibrosis or scarring and detect myocardial infarction (MI) and non-ischemic cardiomyopathy more accurately than conventional CT. In addition, multi-energy CT enhanced the diagnosis of myocardial fibrosis by calculating the ECV fraction. Lee et al. (25) demonstrated that the myocardial ECV fraction determined with dual-energy equilibrium contrast-enhanced CCT was consistent with that of CMR imaging and excellent interobserver agreement in per-subject analysis was observed.

Analysis of LV Function

The quantification of LV function using CCT has been validated in prior studies via comparison with echocardiography and CMR (29). In normal Korean adults, Kang et al. (30) demonstrated that the LV myocardial thickness (septal wall thickness, 1.08 ± 0.18 cm vs. 0.90 ± 0.17 cm; posterior wall thickness, 0.91 ± 0.15 cm vs. 0.78 ± 0.10 cm), LV end-diastolic volume (112.9 ± 26.1 mL vs. 98.2 ± 21.0 mL), LV end-systolic volume (41.7 ± 14.7 mL vs. 33.7 ± 12.2 mL), and mass (145.0 ± 29.1 g vs. 107.9 ± 20.0 g) were significantly greater in men than in women when using 320-detector-row CCT, even though these significant differences disappeared after normalization for body

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**Fig. 3. Infarct imaging using first pass and delayed-enhancement CCT in patient with acute MI in left circumflex territory.** Short-axis MPR images of first pass (A) and delayed enhancement (B) show fixed subendocardial perfusion defect (arrows) and delayed transmural hyperenhancement (arrowheads) in mid-lateral LV wall. Curved MPR coronary CT angiography image (C) shows acute thrombotic occlusion (arrows) of proximal left circumflex artery. Subendocardial perfusion defect indicates microvascular occlusion and poor prognosis. MI = myocardial infarction.
surface area. The measurement of LV functional parameters by CCT can be used as an alternative, particularly in cases of equivocal or suboptimal echocardiography or contraindications for CMR. However, there is not sufficient evidence to recommend CCT as a routine measurement of LV functional parameters (11, 12). A wide-detector CT scanner with single shot scanning or dual-source CT encompassing both cardiac cycles may be used routinely for simultaneous functional analyses.

**Approach for LV Myocardial Diseases**

The evaluation of LV myocardial diseases using the CCT is based on LV volumes and function, regional LV wall motion, LV wall thickness, and myocardial density with and without contrast enhancement (Fig. 4). Generally, image acquisition in CCT is performed in mid-diastole to identify coronary anomalies or stenoses. Accordingly, interpretation of LV diameters and wall thickness may be inadequate, unless correct ECG timing is considered at the point of acquisition. Nonetheless, in the presence of definite morphological abnormalities such as LV wall asymmetry or distinct hypertrophy or thinning, the diagnosis may be apparent even when the acquisition phase is technically incorrect (1).

**LV Wall Thickness**

Measuring LV myocardial thickness is critical for the diagnosis and characterization of many cardiovascular diseases. Normal values for LV myocardial thickness published in the current literature are derived from echocardiography and CMR. The thickness of the myocardium is commonly measured at the interventricular septum at end-diastole. LV trabeculations are excluded from the measurement. The reference range of the LV septal and posterior wall thickness at end-diastole using echocardiography is 0.6–0.9 cm in women and 0.6–1.0 cm in men (31). In normal Korean adults, the mean LV myocardial wall thickness measured on CCT was less than 11 mm at the septum and 10 mm at the posterior wall (30).

**Diseases Associated with LV Wall Hypertrophy**

LVH, defined by the increase in LV mass and LV septal wall thickness, is a common cardiac finding generally caused by a hemodynamic overload. LVH severity is graded based on LV septal wall thickness, indexed LV mass, and LV geometry. The reference values for LVH severity in clinical guidelines, which are based on echocardiographic measurements, are also used for CMR and CCT (31-33).

LVH, frequently defined by interventricular septal and/or posterior wall thickness at end-diastole > 11 mm, is a marker for cardiac disease. LVH is a common pathology which requires exhaustive characterization. The exact diagnosis and differential diagnosis of LVH is of paramount therapeutic and prognostic value. Physiological LVH occurs in athletes (Athlete’s heart). Pathological LVH occurs in athletes (Athlete’s heart). Pathological LVH is mainly classified into the primary (hypertrophic cardiomyopathy; HCM) and secondary types. LVH results in an increased afterload (aortic stenosis [AS], aortic insufficiency, and hypertension) or myocardial infiltration (amyloidosis,

![Fig. 4. Global and regional LV function assessment with CCT in 51-year-old man with previous MI.](image)

Precontrast CCT image (A) shows curvilinear fat deposition in subendocardium of LV myocardium (arrowheads). Short-axis MPR CCT images obtained during end-systole (B) and end-diastole (C) show akinesia, curvilinear fat deposition in subendocardium (arrowheads), and thinned myocardium (5 mm in thickness) in mid-anterior and anteroseptal LV wall (arrows). LV ejection fraction, end-diastolic, and end-systolic volumes were 57%, 137 mL, and 59 mL, respectively.
sarcoidosis, Fabry disease, and cardiac tumors) (33). The basic diagnostic approach for LVH depends on the morphological characteristics of LVH (symmetrical vs. asymmetrical) (Fig. 5).

### Asymmetrical LVH

Isolated basal septal hypertrophy (IBSH) involving at least 15 mm thickness is occasionally termed a sigmoid septum or septal bulge. It is detected in up to 10% of cardiac patients without HCM and is more prevalent in the elderly population (34). In a study by Ranasinghe et al. (35), the presence of IBSH was strongly related to age with the observed frequency rising from 1% of people younger than 50 years to almost 10% in those aged 80–90 years. The frequency of IBSH morphology was 14-fold higher than the frequency of typical morphological forms of HCM, and 65% of patients had a history of hypertension. A few patients with IBSH manifest exertional LV outflow tract (LVOT) obstruction and dyspnea, leading to difficulty in differentiating IBSH from HCM (35). In a study by Gaudron et al. (36) the echocardiographic septal bulge, defined as the basal-septal wall thickness ≥ 2 mm thicker than the mid-septal wall thickness, strongly predicted hypertension with a sensitivity of 93% and specificity of 86%. The septal bulge in patients with hypertension is a very early sign of hypertensive heart disease. The LVOT and basal-to-middle interventricular septum are clearly visualized on 3-chamber and short-axis multiplanar reformatted (MPR) images of ECG-gated CCT (Fig. 6).

### Hypertrophic Cardiomyopathy

HCM is the most common inheritable primary cardiomyopathy that is characterized by unexplained diffuse or segmental LVH without compensatory dilatation of the LV chamber, and with normal or supernormal systolic function (37). Progression to end-stage HCM, known as the burnout or dilated phase, is characterized by systolic dysfunction, LV dilatation, and wall thinning; it occurs in 2.4% to 15.7% of individuals and is associated with largely unfavorable prognosis (38, 39). The usual diagnostic criterion for HCM is LV maximal wall thickness ≥ 15 mm at the end-diastolic phase. Particularly, LV maximal wall thickness ≥ 30 mm is associated with sudden cardiac death (40). The most common form of HCM is asymmetric septal hypertrophy, which is defined as hypertrophy with a septal-to-inferolateral wall thickness ratio ≥ 1.3. Other forms of HCM are focal mass-like, mid-ventricular, and apical (41-43).

CCT is more accurate than transthoracic echocardiography to detect LVH, particularly for the anterior-lateral free wall and for the apex. CCT plays a potential role in the assessment of HCM based on key morphological characteristics, LV systolic
function, the extent of myocardial fibrosis with delayed-enhancement (diffuse or focal enhancement with patchy or massive mid-wall), ECV measurement, and the presence of LV crypts as well as coronary artery evaluation simultaneously (Fig. 7). CCT reveals a thin-walled apical aneurysm showing transmural enhancement and intracavitary thrombus in patients with apical HCM with burned-out phase (42, 43).

Sarcoidosis
Sarcoidosis is a multisystemic disorder of unknown cause that is characterized histopathologically by noncaseous epithelioid granulomas. Granulomas and/or fibrous scars tend to be distributed in the subepicardial layer; however, they can be present anywhere in the myocardium. LVH in a noncoronary distribution is frequent and it mimics HCM with asymmetric focal LVH. Sarcoid lesions ultimately heal through fibrosis, which leads to myocardial thinning and ventricular aneurysm. The myocardial thickness fluctuates according to disease activity, with the myocardium thicker during the active phase and thinner during the healed phase. Thus, it may be difficult to distinguish cardiac sarcoidosis from other cardiomyopathies based on delayed-enhancement pattern and myocardial thickness (44-46). CCT reveals the typical morphological features and delayed-enhancement (multifocal segments with transmural or subepicardial distribution) in cardiac sarcoidosis, as well as its involvement in other organs (Fig. 8) (47).

Cardiac Tumor
Primary or secondary tumors located in the left ventricle lead to localized LVH. Primary cardiac tumors are rare, and the histological types are varied. The incidence of metastatic cardiac tumors is 100-fold more common than that of primary tumors. Myocardial involvement is a less
common site of cardiac metastasis (Fig. 9). Benign cardiac tumors such as fibroma and rhabdomyoma are homogeneous masses with soft tissue attenuation, smooth and well-defined margins without infiltration. However, malignant tumors such as rhabdomyosarcoma and angiosarcoma show lobular, ill-defined, and invasive borders and a broad attachment to the myocardium. Primary cardiac lymphomas with massive myocardial infiltration may show irregular thickening of the LV wall that mimic classic HCM (48). CCT may facilitate the differentiation between cardiac tumor of the LV myocardium and mass-like HCM.

**Symmetrical LVH**

Sports-Related LVH: ‘Athlete’s Heart’

The term ‘athlete’s heart’ refers to a clinical picture characterized by a lower heart rate and cardiac enlargement. Long-term exercise training-induced hemodynamic changes lead to an increase in both LV dilation and LVH, in order to normalize LV wall stress. Accordingly, athlete’s heart

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**Fig. 8. Cardiac sarcoidosis in 61-year-old woman with irregular cardiac rhythm and dyspnea.**

Short-axis MPR CCT images obtained during early (A) and delayed (B) contrast-enhancement phases show concentrically hypertrophied mid-LV wall in mid-diastole with diffuse transmural and mesocardial delayed enhancement (arrows). Delayed-enhancement CMR image (C) shows diffuse mesocardial enhancement in septum and multifocal patchy mesocardial enhancement in mid anterior, lateral, and inferior LV wall (arrows). Delayed-enhancement CMR is superior to delayed-enhancement CCT for differentiating patterns of delayed myocardial enhancement. CMR = cardiovascular magnetic resonance.

**Fig. 9. LV metastasis from lung cancer in 93-year-old man.**

Contrast-enhanced chest CT image (A) shows 13-mm lobulated nodule with heterogeneous enhancement in anterior segment of left lower lobe (arrow). Mid-diastolic short-axis MPR CCT image (B) shows large infiltrating mass with homogeneous hypoenhancement as focal hypertrophied mid inferoseptal and inferior LV wall (arrows).
can mimic diseases such as HCM or dilated cardiomyopathy (DCM). In elite athletes, the LV end-diastolic diameter is not frequently increased to > 60 mm (49). In 947 elite athletes, the maximal end-diastolic septal wall thickness was ≤ 12 mm in most (50). CCT may be used to rule out coronary anomalies or coronary artery diseases (CAD) in symptomatic athletes (51).

Hypertension
Hypertension is a highly prevalent cardiovascular risk factor and it is the most common cause of LVH. Echocardiographic LVH is detected in 20–40% of patients with hypertension. Hypertensive heart usually shows concentric LVH, which is characterized by normal cavity size, uniformly increased LV wall thickness and increased LV mass. Interventricular septal thickness increases up to 15 mm. Left atrial dilatation is also seen in hypertension (52, 53). In a study by Rodrigues et al. (54), an asymmetric end-diastolic wall thickness of ≥ 15 mm and > 1.5-fold the opposing myocardial segment in ≥ 1 segment was exclusively observed in the basal-to-mid septum in 21% of a purely hypertensive cohort. CCT is appropriate for LV wall thickness, mass and volume measurement, and for excluding CAD in patients with hypertension.

Aortic Stenosis
AS is the most common valvular heart disease (VHD) in the elderly population. AS increases LV afterload and causes compensatory LVH (concentric LVH). LVH causes reversible myocardial ischemia and irreversible myocardial injury, such as interstitial myocardial fibrosis (55). Accordingly, it is increasingly clear that it is also a disease of the left ventricle rather than the aortic valve exclusively. Usually, the LV wall is symmetrically hypertrophied in AS and, occasionally, an area of the LV shows asymmetrical septal hypertrophy (Fig. 10) (56). In a study by Tuseth et al. (57), asymmetrical septal hypertrophy (defined as interventricular septal/posterior wall thickness ratio > 1.5 on echocardiography) was found in 22% of 1719 patients with asymptomatic AS and hypertension was the most important predictor of asymmetrical septal hypertrophy and asymmetric LVH.

CCT is a useful imaging modality for severe AS patients indicated for transcatheter aortic valve replacement. The assessment of LV function and scar imaging of the myocardium with CCT has not been routinely established in clinical practice (56). Recently, Bandula et al. (24) demonstrated a significant correlation between both equilibrium CT–derived and equilibrium CMR imaging–derived ECV and percentage of histological fibrosis in patients with severe AS. Equilibrium CT–derived ECV was significantly correlated to equilibrium CMR imaging–derived ECV.

Amyloidosis
Amyloidosis is a systemic disease characterized by the extracellular deposition of pathological and insoluble amyloid protein in multiple organs. Approximately 50% of patients with immunoglobulin light-chain amyloidosis develop cardiac involvement. Cardiac amyloidosis is associated with poor prognosis. Myocardial thickening with a restrictive diastolic filling pattern is pathognomonic of cardiac amyloidosis. A diffusely heterogeneous delayed
hyperenhancement along the areas of amyloid protein deposition, predominantly affecting the subendocardium and the basal segments, is more specific than the morphologic and functional findings (58, 59). CCT reveals thickening and subtle lower attenuation of the ventricular wall without dilatation. Subendocardial and circumferential delayed-enhancement is apparent on delayed-enhancement CCT (Fig. 11) (47). In a study by Deux et al. (60), myocardial attenuation on delayed-enhancement CCT was higher in patients with cardiac amyloidosis (121 ± 39 HU) than in control patients (81 ± 17 HU). Dynamic equilibrium CT recently showed that the ECV was higher in patients with amyloidosis than with AS (0.54 ± 0.11 vs. 0.28 ± 0.04, \( p < 0.001 \)) with no overlap and the ECV tracked clinical markers of cardiac amyloid severity (6). Accordingly, CCT, like CMR, has a potential role in the non-invasive diagnosis and quantification of cardiac amyloidosis.

**Diseases Associated with LV Wall Thinning**

Myocardium thinning is one of the principal signs of myocardial damage and ischemia. Even though old MI is the most common disease characterized by focal LV myocardial thinning, normal anatomical and congenital LV wall thinning and other non-coronary heart diseases also exhibit focal LV myocardial thinning (1). Several studies have focused on the presence of focal thinning as nonviable scar tissue in conventional cardiac imaging (61, 62). CCT facilitates the differential diagnosis of LV myocardial thinning based on the location, asynergy, and presence of fibro-fatty changes of thinned LV sites (Fig. 5) (63).

**Global LV Wall Thinning**

Dilated cardiomyopathy

DCM, the most common form of non-ischemic cardiomyopathy, is characterized by a dilated and poorly functioning left ventricle in the absence of CAD, pressure overload, or infiltrative cardiomyopathies. Half of the cases are idiopathic in nature, with the remainder secondary to previous infection, alcohol and drug abuse, or toxicity. Sudden cardiac death, which accounts for 10% of all adult sudden cardiac death cases, may be the first manifestation of idiopathic DCM (64).

LV dilatation is a key finding of DCM and is occasionally associated with right ventricular dilatation and hypertrabeculation of both ventricles. The thickness of the LV wall increases or decreases to compensate for the dilatation. Occasionally, intracavitary thrombi are present in the ventricles. Three types of DCM-related delayed-enhancement include mid-wall, subendocardial, or transmural. The absence of delayed-enhancement has also been reported (65, 66). CCT has been used to evaluate the biventricular volumes, wall thinning (diastolic wall thickness < 5.5 mm), ventricular mass, and global and regional LV functions using the multiphase reconstruction of cine images (Fig. 12). Furthermore, CCT allows for the characterization of the myocardium and the differentiation of DCM patients from LV dysfunction related to CAD by providing myocardial delayed-enhancement pattern and ECV values of the myocardium (25, 47).

**Non-Compaction Cardiomyopathy**

Non-compaction cardiomyopathy (NCC) is characterized by the presence of an abnormal noncompacted myocardium due to the arrested development of endomyocardial compaction. Its prevalence is 0.05% in the general population (67). The morphological findings of NCC are numerous and manifest as prominent trabeculations and deep inter trabecular recesses that communicate with the LV cavity but not with the coronary arteries (68, 69). The most frequently involved segments include the apical and mid-ventricular areas of the inferior and lateral walls of the left ventricle.
ventricle. The high spatial resolution of CCT facilitates clear depiction of trabeculations along the LV wall and LV crypt thrombus and it also facilitates an accurate measurement of the end-diastolic thickness of the noncompacted and compacted myocardium perpendicular to the compacted layers of the LV wall (Fig. 13) (70). Melendez-Ramirez et al. (71) demonstrated that the presence of a non-compacted-to-compacted ratio ≥ 2.2 in ≥ 2 myocardial segments is diagnostic of NCC. The thickness of the compacted layer was significantly lower in the segments with NCC compared with the segments without it.

**Localized LV wall Thinning**

**Myocardial Infarction**

MI is a major cause of death and disability worldwide (72). The primary cause of acute MI is the sudden disruption of an unstable atherosclerotic plaque in the coronary artery followed by acute intracoronary thrombosis. The infarct progresses from the subendocardium towards the epicardium in a wavefront pattern, which may eventually become transmural. Regional wall thinning is indicative of transmural MI which affects the full thickness of the affected muscle segments (73).

Non-contrast CCT facilitates the detection of chronic MI displaying fatty replacement with lower attenuation (HU < 0) or myocardial calcification in chronic MI territories. Ichikawa et al. (74) demonstrated the presence of adipose tissue in the LV wall (94% subendocardium) of the region perfused by the infarct-related artery in 33 of 53 MI patients (62%) and identified a significant relationship with infarct age in patients with previous MI, particularly among patients with infarct age ≥ 3 years. Early-phase contrast-enhanced CCT shows hypoenhancement due to the reduced distribution of contrast medium during the first passage in infarcted areas of patients with acute, chronic, and subacute MI. Remodeling of the left ventricle, focal wall thinning, regional LV wall motion abnormality, or LV thrombus or aneurysm may be easily apparent on early-phase CT (75, 76). Simple measurement of end-diastolic wall
thickness (< 6 mm) indicates irreversible myocardial damage and obviates the need for viability testing such as delayed-enhancement CMR (77). Nieman et al. (78) demonstrated a significantly lower CT attenuation in patients with chronic MI (-13 ± 37 HU) compared with those with acute MI (26 ± 26 HU) and normal controls (73 ± 14 HU, \( p < 0.001 \)). The attenuation difference between infarcted and remote myocardium was larger in patients with chronic MI than in patients with recent MI. In addition, chronic MI was associated with wall thinning and ventricular dilation, whereas recent MI was not. Cury et al. (79) showed that comprehensive CT analysis for the detection of acute MI, based on matching perfusion defect and abnormal regional wall motion, yielded a sensitivity of 94% and a specificity of 97% and showed that the interobserver reliability was better with CT when compared with transthoracic echocardiography.

Delayed-enhancement CCT ranging from 5 to 15 minutes after the contrast injection led to an accurate estimation of infarct size and microvascular occlusion in acute MI (80). Sato et al. (81) demonstrated that the size of myocardial-delayed enhancement on CCT images obtained immediately after primary percutaneous coronary intervention was a significant and independent predictor of cardiac events after adjustment for Thrombolysis In Myocardial Infarction risk score, LV ejection fraction, total defect score on single-photon emission CT with technetium tetrofosmin, and transmural extent of delayed-enhancement on CCT. The feasibility and short examination time of CCT are considered important advantages when compared with CMR.

LV Aneurysm

LV aneurysm is defined as an outpouching containing full thickness of the LV wall with thin, abnormally contracting and scarred myocardium with its characteristic paradoxical bulging or dyskinesia. LV aneurysm most frequently develops after transmural MI, usually involving the apical, the anterior, or the anterolateral wall (left anterior descending artery territory). CCT findings include broad neck (the ratio of the maximum diameter of the orifice to the maximum internal diameter of the cavity = 0.9–1.0), smooth transition from normal myocardium to thinned scarred myocardium (delayed-enhancement), and paradoxical expansion or dyskinesia. In addition, fatty replacement of the infarcted myocardial wall, calcification, and intraventricular thrombus formation may be seen in chronic aneurysms (Fig. 14). A true aneurysm has a lower risk of rupturing when compared with a pseudoaneurysm and it is often managed medically (82, 83).

LV Pseudoaneurysm (a false aneurysm)

It is defined as an outpouching that results from rupture of the LV free wall, limited by an overlying adherent pericardium without a myocardial layer. Pseudoaneurysms are most often attributed to MI following left circumflex coronary artery occlusion. However, it may also occur after cardiac surgery, trauma, or infection (84). Morphologically, pseudoaneurysms are characterized by a neck narrower than the diameter of the aneurysm (the ratio of the maximum diameter of the orifice to the maximum internal diameter of the cavity = 0.25–0.5), an abrupt transition from normal myocardium to aneurysm, and a distinct discontinuity of the ventricular wall. Generally, the inferior and lateral wall segments are involved (Fig. 15). Pseudoaneurysms have poor prognoses because of a high risk of rupture, thus warranting urgent surgical repair. CCT can distinguish between pericardium, thrombus, and the myocardium and it can identify akinetic/dyskinetic segments in the LV wall and provide diagnostic clues for LV aneurysms and pseudoaneurysms (83, 85).

LV Apical Thin Point

The LV apex is the thinnest part of the LV myocardium
in normal and hypertrophied hearts and it is different from
the cardiac apex (Fig. 1A) (86). Apical thickening is not
observed throughout the entire cardiac cycle. This extreme
tip of the apex is difficult to visualize on echocardiography
but is clearly visible on CCT. In a study by Johnson et al.
(87), the average thickness of the LV apical thinning was 1.2
mm in 64 patients using a 64-slice CT scanner. This normal
anatomical thinning should not be confused with either a
myocardial scar from an ischemic insult or a congenital LV
diverticulum.

LV Crypts
Myocardial crypts are defined as narrow, deep blood-
filled invaginations in the compact LV myocardium with a
penetration > 50% of the thickness of adjoining myocardium
during diastole and are almost or completely obliterated
by surrounding tissue during systole. They commonly
involve the basal and middle segments of the infersetial
LV myocardium, as well as the basal inferior wall and are
reported in a wide variety of cardiac diseases as well as in
normal control subjects (Fig. 16) (88). In a study by Child
et al. (89), crypts were found more frequently in patients
with hypertensive cardiomyopathy (27%) and HCM (11.7%)
than in normal control subjects (3.6%). Recent studies
suggest that the presence of crypts in patients with an
otherwise normal CMR and a family history of HCM was
a predictor of ‘gene carrier’ status, with implications for
genetic testing (90, 91). CCT is a highly sensitive imaging
tool for the detection of myocardial crypts with MPR images
from the isotropic volumetric data set covering all portions
of the left ventricle.

Congenital LV Diverticulum
Congenital LV diverticulum is a rare cardiac malformation
(approximately 0.04% in the general population). Despite
the absence of symptoms, this malformation may be associated with systemic embolization, fatal ventricular arrhythmias, and sudden death due to ventricular rupture (92). Based on its location, this malformation can be classified as fibrous or muscular. The muscular diverticulum is more frequent and mostly found in the apical region. It is characterized by a finger or hook-like pouch of the entire LV myocardial wall with synchronous contractility (Fig. 17). The fibrous diverticulum is usually located either in the base of the heart or in the subvalvular area. It is characterized by an outpouching with a narrow neck, no volume change during the cardiac cycle, and the presence of fibrous tissue on the diverticulum wall. CCT facilitates accurate diagnosis of LV diverticulum based on the location, tissue characteristics, and contractility of LV outpouching (93).

Myocarditis

Myocarditis is an acute or chronic inflammatory disease of the myocardium. It is an important etiology underlying other myocardial diseases such as DCM and arrhythmogenic right ventricular cardiomyopathy. Direct myocardial injury is accompanied by edema, necrosis, and regional or global contractile dysfunction. The late post-inflammatory fibrotic phase shows scar formation and irreversible damage to the LV wall, as well as LV dilatation (Fig. 18) (94-97).

In patients with acute chest pain, CCT may be used to exclude CAD. Delayed-enhancement CCT shows delayed hyper-enhancement that is transmural, subepicardial or confined to small foci within a layer of the myocardium. Delayed-enhancement CT correlates with CMR in acute myocarditis based on areas and degrees of involvement. A reduced tube voltage increases the contrast of iodine and simultaneously lowers radiation exposure (98, 99).

Myocardial Fat

Adults generally display a varying amount of myocardial fat without cardiac disease. Physiological myocardial fat increases with age and it is considered as part of the normal aging process. Cardiac physiologic fat occurs predominantly in the right ventricle affecting its anterolateral free
wall and outflow tract. Occasionally, the LV apex and trabeculae may be affected with small fatty foci (Fig. 19). CCT facilitates incidental detection of myocardial fat on source axial images of submillimeter thickness and aids the differentiation of pathologic from physiologic fat according to the characteristic fat patterns, leading to accurate diagnosis (100).

Recognition of patient age, characteristic locations of myocardial fat, myocardial thickness, and ventricular size facilitate the differentiation of physiological and pathological myocardial fat in cardiac imaging. Following MI, the scar tissue is progressively replaced by fat (lipomatous metaplasia). The fatty replacement is associated with infarct age and is frequently seen in infarctions older than three years but is absent in patients with less than 6-month-old infarcts. CT analysis shows that the prevalence of LV myocardial fat is 22–62% among patients with a history of MI. Non-enhanced or contrast-enhanced CT images show that myocardial fat associated with a healed MI is an area of linear or curvilinear subendocardial low attenuation in the culprit coronary artery, frequently in the LV. It is mostly located in the subendocardial myocardium. LV myocardial fat is also associated with myocardial thinning or calcification. LV myocardial fat in arrhythmogenic right ventricular cardiomyopathy appears as a wedge-shaped or bandlike configuration in the subepicardial LV-free wall on CT.

Cardiac lipoma is a benign encapsulated tumor with mature adipose tissue and is usually located in the myocardium of any cardiac chambers as an asymptomatic fatty mass. DCM may also be associated with myocardial fat deposition in 18–24% of cases (74, 101-103).

CONCLUSION

The distinction between various LV myocardial diseases is of great significance as the management options vary considerably with the prognosis. Their characteristic features in various imaging modalities show considerable overlap. In many forms of myocardial disease, thickening and/or thinning of the LV myocardium with fibrosis is a common feature. CCT is inferior to CMR in differentiating myocardial diseases and myocardial fibrosis, except myocardial fat. Especially, most of the restrictive myocardial diseases can be normal on CCT. However, the higher spatial resolution and volumetric acquisition of CCT allows for the depiction of myocardial fat and morphological abnormality and has a promising role in the diagnosis of diseases affecting the LV myocardium. Recently, myocardial delayed-enhancement CCT and multi-energy CCT have yielded promising results in the detection and characterization of various LV myocardial diseases. CCT has potential as an adjunct to echocardiography and CMR in the diagnosis of LV myocardial diseases in a single sitting.

Conflicts of Interest

The authors have no potential conflicts of interest to disclose.

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