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Poly(β-L-malic acid) (PMLA) is a natural polyester produced by numerous microorganisms. Regarding its biosynthetic machinery, a nonribosomal peptide synthetase (NRPS) is proposed to direct polymerization of L-malic acid in vivo. Chemically versatile and biologically compatible, PMLA can be used as an ideal carrier for several molecules, including nucleotides, proteins, chemotherapeutic drugs, and imaging agents, and can deliver multimodal theranostics through biological barriers such as the blood–brain barrier. We focus on PMLA biosynthesis in microorganisms, summarize the physicochemical and physiochemical characteristics of PMLA as a naturally derived polymeric delivery platform at nanoscale, and highlight the attachment of functional groups to enhance cancer detection and treatment.

Biopolymer: From Benchtop to Bedside
PMLAs are water-soluble polyesters with repeating malyl units (see Glossary) that were discovered in aqueous extracts of Penicillium cyclopium culture in 1969 [1]. To date, three major types of PMLAs have been identified that differ in their ester bonds between hydroxyl groups and either α- or β-carboxyl groups in the polymeric chain, namely α-, β-, and α,β-PMLAs (Figure 1A). However, naturally available PMLA, such as from Aureobasidium pullulan or Physarum polycephalum, has a β-type structure, whereas α- and α,β-PMLAs are obtained by chemical synthesis [2].

In addition to functions in carbon storage and as an energy reservoir for other polyhydroxyalkanoates (PHAs) in their host microorganisms [3], PMLA acts as a molecular transporter to bind to and carry nuclear proteins related to DNA replication, demonstrating its unique role in maintaining protein homeostasis and assisting DNA synthesis [4]. Unlike bioderived water-insoluble polyhydroxybutyrate (PHB), PMLA possesses a high capacity to attach hydrophobic molecules while remaining water-soluble owing to the exceptional hydrophilicity of abundant carboxylic acids that are present as pendant groups from its polymeric chain [5–7]. This characteristic of PMLA diminishes its innate toxicity and immunogenicity, and makes it compatible with various biological systems [8–10]. Moreover, hydrolyzable ester bonds in the backbone of the polymeric chain facilitate the complete decomposition of PMLA in biological milieu, where the sole end-product of malates is reused by the citric acid cycle in the mitochondrial matrix as a part of central cellular metabolism [11]. Only the L-form of malic acid is obtained naturally via microbiological production [12] (Figure 1A). Non-enzymatic hydrolysis of PMLA takes place via spontaneous random breakdown of ester bonds and concurrent formation of intermediate oligomers, whereas enzymatic hydrolysis in the presence of PMLA hydrolases (Box 1) uncaps one unit of malic acid after another from one end (the hydroxyl terminus) of the polymeric chain to the other [13]. The PMLAs discussed in this review focus on biogenic poly(β-L-malic acid), although synthetic PMLAs are discussed where relevant.

Highlights
Genome-wide analyses have recently been used to map the genes encoding PMLA synthetase in different microorganisms. High-grade production of PMLA from fermentation by fungi or myxomycetes enables increasing applications of this biodegradable polymer in medical research.

PMLA-based nanoconjugates can successfully penetrate the blood–brain barrier in rodent models, thus delivering imaging and/or therapeutic reagents to intrabrain targets and showing great potential for treating neurological disorders in human.

With unmatched compatibility and resorbability, biosynthetic PMLAs are good examples of future macromolecular compounds generated by a green and sustainable approach, eventually benefiting human health.
Given its great sustainability because it is produced from natural sources, PMLA serves as a platform for potential multimodal conjugates with unmatched bioavailability, biocompatibility, and biodegradability. For this reason, PMLA has been intensively and extensively used in biomedical and medicinal research, particularly in drug delivery and in bioimaging for cancer theranostics [14,15].

### Biosynthesis of PMLA in Different Microorganisms

Following its discovery in *P. cyclopium* as an acidic substance containing no nitrogen (molar mass M = ~5000 g/mol), PMLA was also found in the myxomycete *P. polycephalum* (M = 10 000–12 000 g/mol) as an inhibitor to DNA polymerases, and in the yeast-like fungi *Aureobasidium* sp. (M = 6000–11 000 g/mol) and *A. pullulan* (M = 3000–5000 g/mol) as an extracellular secretion in culture broth [16,17]. Bacteria producing PMLA have not yet been identified. A study that examined PMLA bioproduction from 56 strains of *A. pullulan*...
of a diversity of phylogenetic clades indicated high productivity but low molar mass (5100–7900 g/mol), where PMLA was bound to polysaccharides of varying molar mass depending on the exact strain type [17]. By screening various Aureobasidium spp. and optimizing the culture conditions, efforts have been made to obtain efficient biosynthesis of PMLA with high molar mass (up to 20 000 g/mol) [18]. Using a highly productive Aureobasidium sp. strain isolated from mangrove systems, purified PMLA with M = 205 400 g/mol was reported [19]. By contrast, PMLA produced from the plasmodial stage of P. polycephalum sustains a much elongated linear chain in its pure form, with M = 30 000–300 000 g/mol [12,20].

**Generic Biosynthetic Pathways of PMLA**

Using D-glucose as the most efficient carbon source, and relying on nutrients available in the extracellular culture medium, independent extramitochondrial and intramitochondrial metabolic routes for generating L-malate (the immediate precursor to PMLA) in vivo were unraveled [21] (Figure 2). On the one hand, in the presence of exogenous carbonates (e.g., CaCO₃ or Na₂CO₃), L-malate is produced via a reductive pathway in the cytoplasm; because of the high level of CO₂ in the cytoplasm, pyruvate is prioritized for carboxylation to oxaloacetate by pyruvate carboxylase, and this is further reduced by malate dehydrogenase to malate [22]. Alternatively, in a similar manner, phosphoenolpyruvic acid is directly converted by phosphoenolpyruvate carboxylase to oxaloacetate, forming malate [23]. Therefore, phosphoenolpyruvic acid and pyruvate from the glycolysis pathway are indispensable molecules for malate synthesis in vivo, whereas their carboxylases govern carbon flux for malate biosynthesis because regulated carboxylase activity influences the ultimate level of PMLA bioproduction [23,24].

On the other hand, if exogenous carbonates are absent, malate formation via the oxidative pathway is mostly achieved in the mitochondrial matrix through either the tricarboxylic acid (TCA) cycle or the glyoxylate bypass [25]. Glucose or another sugar is transformed into pyruvate through glycolysis, followed by import into mitochondria by mitochondrial pyruvate carrier (MPC) proteins and subsequent decarboxylation by pyruvate decarboxylase complex to produce acetyl coenzyme A (acetyl-CoA), thus entering the TCA cycle and being converted to four-carbon oxaloacetate and subsequently to six-carbon citrate [26,27]. The TCA cycle continues as a series of biochemical transformations that take place in an enzyme-mediated cascade, generating products including cis-aconitate, isocitrate, α-ketoglutarate, succinate, fumarate, malate, and

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**Box 1. PMLA Hydrolases as Opponents of Biosynthesis**

PMLA hydrolases (also called PMLA depolymerases or polymalatas) have been purified and characterized from both eukaryotic and prokaryotic microorganisms [73,76]. In eukaryotes, particularly PMLA-producing myxomycetes, soluble PMLA hydrolase serves as a molecular chaperone of PMLA and binds to its hydroxyl terminus at the penultimate malyl residue for catalytic cleavage, although another binding site 12 malyl residues down the polymeric chain was also proposed to govern stability and carriage function (Figure 1B) [73]. Intracellular PMLA hydrolase remains inactive and forms complexes with PMLA that may carry other nuclear proteins, assisting the translocation of PMLA into the nucleus while leaving PMLA hydrolase on the surface of nuclear envelope, possibly because of either its binding to envelope proteins and/or the outer nuclear membrane, or disruptive variation in local ionic strength (Figure 1C) [78]. After discharging its nuclear protein cargo, PMLA exits through nuclear pores and to join newly synthesized PMLA in the cytoplasm for the next deliveries [78]. PMLA thus shuttles between the nucleus and the cytoplasm to maintain homeostasis in different phases of the cell cycle. Excess PMLAs bound to hydrolases are excreted through the cell membrane, where a membrane-bound tyrosine kinase then phosphorylates PMLA hydrolases and activates their hydrolytic activity, leading to degradation of concomitantly released PMLAs in the culture medium (peak activity at pH 3–5) [74]. However, the hydrolases may differ across different eukaryotes such as PMLA-producing myxomycetes and fungi: PMLA isolated from P. polycephalum had higher molar mass and polydispersity than that from A. pullulan [38]. In prokaryotes such as bacteria that are devoid of PMLA, insoluble PMLA hydrolases are confined to the outer cell membrane where they hydrolyze outsourced PMLA into malic acid monomers that are further taken up for cellular metabolism [76]. Unlike PHB depolymerase, PMLA hydrolase does not exhibit serine esterase activity in which a nucleophilic serine in the active site initiates substrate hydrolysis, and is not inhibited by serine protease inhibitors [78].
eventually oxaloacetate again. In parallel, taking a shortcut in the TCA cycle, a process known as
the glyoxylate shunt, isocitrate is directly converted into glyoxylate and succinate; glyoxylate then
reacts with acetyl-CoA to produce malate, and succinate generates malate catalyzed by succi-
nate dehydrogenase and fumarase [28]. The glyoxylate pathway could thus be driven to produce
a malyl-AMP ligase and an unknown PMLA polymerase, in conjunction with an auxiliary peptide or enzyme (e.g., spherulin 3b in P. polycephalum) [30,39].

Because the inner membrane of mitochondria remains a barrier to most molecules, malate and
oxaloacetate from the oxidative TCA cycle or glyoxylate shunt interchange with their counterparts
in the cytosolic reductive pathway via the malate/aspartate shuttle, where oxaloacetate is reduced
to malate both extramitochondrially and intramitochondrially to permit transportation and avoid
oxaloacetate accumulation in the cytoplasm [21]. In cultures of P. polycephalum and A. pullulan,
the addition of exogenous carbonates augments CO2 fixation and pyruvate carboxylation into ox-
alocetate by pyruvate carboxylase in the cytoplasm, abolishing the intramitochondrial pathways for
L-malate production and ensuing PMLA synthesis (Figure 2) [23,30]. Under these conditions, the
addition of TCA cycle metabolites into the cell culture might not promote PMLA production [11]. In other words, environmental carbonate works as a switch between oxidative and reductive pathways to produce malate. Furthermore, carbonate adjusts the acidity of the culture medium, noting that low pH values accelerate PMLA hydrolysis. In contrast to *P. polycephalum*, that merely uses D-glucose as a carbon source in malate and PMLA bioproduction, *A. pullulan* takes up a broad spectrum of saccharides (e.g., sucrose, fructose, and maltose) because it expresses a remarkable diversity of polysaccharide lyases, glycoside hydrolases, carbohydrate esterases, glycosyltransferases, and sugar transporters, enabling its efficient utilization of diverse carbohydrates to produce malate [31–33]. By depleting the nitrogen supply or augmenting the carbon/nitrogen ratio in the cell medium, PMLA bioproduction is significantly enhanced per unit of cell mass because nitrogen starvation upregulates the expression of key enzymes in PMLA biosynthetic pathways, uncoupling cell growth from PMLA production [34,35].

At the cost of ATP probably derived from glycolysis, malates are polymerized to form PMLA in the cytoplasm [36]. The acellular slime mold *P. polycephalum* only synthesizes PMLA in its multinucleated plasmodia, whereas the yeast-like fungus *A. pullulan* spends its entire life cycle (except hyphae form) producing PMLA [37,38]. Although the search for PMLA synthetase is still underway, a nonribosomal peptide synthetase (NRPS) machinery was proposed that first forms malyl-AMP via the action of malyl-AMP ligase, and this is then assembled into a polymeric chain by an unidentified polymerase [36]. In addition, a plasmodium-specific polypeptide spherulin 3b (i.e., NKA48) was found to assist PMLA synthesis, although similar enzymes have not been identified in fungi [39]. Alternatively, in *A. pullulan*, it was proposed that cytosolic malate may be polymerized into PMLA using malyl-CoA as the precursor, followed by the action of malate-CoA ligase and PMLA synthetase [40]. In one variety of *A. pullulan*, namely *Aureobasidium melanogenum*, a characteristic NRSP was recently reported to be a putative PMLA synthetase that contains an adenylation domain for ATP binding and malyl-AMP formation, an activatable thiolation domain for phosphopantetheine attachment and polymerization of malyl-AMP into PMLA, and a hexa-transmembrane region for transport of PMLA out of the cytoplasm [41]. Because the whole-genome sequences of several PMLA-producing fungal strains have been determined, a conserved PMLA synthetase across species is expected to be unmasked in the near future [22,42].

**Non-Enzymatic Degradation of PMLA**

Biosynthetic PMLA in aqueous solution (2% w/v) has a pH of 2.0 but a pKₐ of 3.4–3.6 (average M = 10 000–24 000 g/mol) [43]. At acidic pH less than the pKₐ (e.g., pH 2–3), PMLA remains protonated, promoting the formation of intramolecular double hydrogen bonding between side-chain carboxylic acids and the construction of dense, inflexible, double-stranded segments [44]. In phosphate buffer (pH 7.4) at 37°C, PMLA with fully ionized carboxylic groups retains an open-coil conformation owing to the negatively charged neighboring side-chains, and undergoes hydrolysis with a half-life of 10 h, initially following first-order kinetics, whereas elevated temperature and acidic pH dramatically accelerate its hydrolytic degradation [37,45,46]. Moreover, random hydrolysis prioritizes the breakdown of intrachain ester bonds over those at the ends of the molecule, producing oligomers instead of malates until hydrolysis proceeds to completion, whereas hydrophobic substitution (e.g., alkylation) of PMLA side-chains delays this hydrolytic degradation, possibly because of limited water access to ester bonds in the backbone as the polymer conformation alters [47,48]. In addition, a larger substituent group or a higher degree of substitution in the side-chain that increases hydrophobicity, leads to the slower degradation in aqueous solutions [47,48].

**Physiochemical Properties of PMLA**

In a pilot study, repeated intraperitoneal injection of synthetic PMLA into rabbits returned no detectable immune response, demonstrating non-immunogenicity, whereas the same injection into
mice revealed nearly no acute toxicity (LD$_{50}$ = 3.3 g/kg body weight) [49]. Intravenous (i.v.) injection of PMLA sodium salt into mouse tail vein, with repetitive administration at low dosage, showed no mortality or adverse effects at doses up to 3 g/kg body weight; however, mice only tolerated a one-time i.v. high-dose injection (up to ~2 g/kg body weight or otherwise) toxicity was due to the hyperosmolarity of the concentrated polymer solution injected rather than to the polymer concentration per se [50]. The elimination of injected PMLA from blood was very fast, with a $t_{1/2}$ of 8 min or much less, and injection might not even be complete before the polymer is exported into urine [50,51]. Indeed, 70% of injected PMLA was excreted after 1 h, and 90% after 6 h, although there was low but persistent liver accumulation 24 h after injection, yet no substantial accumulation in other organs, including kidney, lung, intestine, spleen, heart, muscle, and brain [50,51]. Notably, these early studies on the pharmacokinetics and biodistribution of synthetic PMLA laid a solid foundation for recent preclinical research using natural PMLA as a pharmaceutical carrier [20]. Bioproduced PMLAs possess a similar or even superior biocompatibility profile to synthetic PMLAs, and their end-product is only L-malic acid. Intriguingly, L-malate administered i.v. into the tail vein in mice had a half-life of only 10 min, and one third of injected dose ended up in exhaled CO$_2$, whereas the majority of the remainder accumulated in tissues via renal tubular reabsorption, participating in the TCA cycle [51].

**Permeation of Cellular Membrane by PMLAs**

PMLA is negatively charged at pH 7.4, and hence poses no disruptive threat to phospholipid membranes because they have the same charge. Given that there is no specific cell-surface receptor of PMLA, water-soluble PMLA is transported into the cytoplasm through the invagination of cell membrane via a process of non-specific endocytosis, although the efficiency of transmembrane transport can be very low. In contrast to PMLA, its copolymers with lipophilic ligands undergo hydrophobic interactions in aqueous solution and assemble into lipophilic patches, and these can interact with the cell membrane, leading to anchoring of lipophilic patches in close proximity to lipid bilayers [52]. Depending on the attached hydrophobic ligands, three distinct mechanisms have been proposed by which different PMLA-conjugated copolymers can induce membrane permeation (Figure 3); these are discussed in the following text:

(i) The carpet model is typified by PMLA leucine ethyl ester (PMLA-LEt$_{H100-x}$) [53]. At physiological pH, esterification of carboxylic acid groups in PMLA side chains leads to permanent charge neutralization, excluding further protonation even when the environmental pH drops. Upon binding to the cell membrane, PMLA-LEt$_{H100-x}$ orients itself to insert the hydrophobic LEt side chain into the phospholipid layer, leaving the outer membrane surface expansively covered by the hydrophilic backbone of the polymeric chain. The hydrophobic binding energy is sufficient to strongly bend the plasma membrane into a curved structure, creating a transient pore that enables membrane permeation [54,55]. This process is independent of pH and its membranolytic efficiency varies according to the ratio of hydrophobic/hydrophilic moieties (Box 2) in the polymer (i.e., $\text{molar fraction}$).

(ii) The belt model is typified by PMLA tritryptophan (PMLA-WWW$_{H100-x}$) [56]. Tritryptophan contains three side-chain indoles and one terminal $\alpha$-carboxylic acid, constituting a non-polar hydrophobic tripeptide. At pH 7.4, the terminal $\alpha$-carboxylic acid in the side chain is deprotonated and ionized; this would be repelled from the cell membrane, but, because of strong hydrophobic interactions, indole in the side chain can attract and intercalate into phospholipids, generating PMLA tritryptophan–lipid complexes and releasing binding energy to stabilize the structure. In another scenario, pH reduction from neutral to acidic may protonate (and neutralize) the end-group carboxylate in the side chain, whereas protonation of the indole moieties is constrained because this would lead to loss of aromatic stabilization. Under both circumstances, the PMLA backbone is sandwiched between two layers of
Mechanisms by which different types of PMLA-based polymers induce cell membrane permeation [53,56]. (A) The carpet model: PMLA polymers first bind to the cell membrane and generate a layer of polymers in which their hydrophobic side chains are inserted into the phospholipid; this is followed by induced curvature of the plasma membrane, forming a transient pore. (B) The belt model: anionized PMLA polymers are first repelled from the cell membrane, but strong interactions between
phospholipids inserted with outflanking tryptophans, forming a 'belt-like' or 'dental brace' configuration [56]. The pH-dependent charge neutralization of the carboxylic acid end-groups does not hamper strong hydrophobic interactions between indole and membrane lipids, thereby leading to pH-independent membrane permeation. This permeation thus resembles the 'boomerang model' that was proposed to mediate viral membrane fusion with the host cell [57]. A highly conserved tryptophan-rich domain has been found in many human viruses, including coronavirus, influenza virus, and HIV, and has been proposed to be a key determinant of viral entry through strong interactions between the aromatic rings of the tryptophan-rich domain and lipids in the target membrane lipid, thus perturbing the lipid bilayer and mediating membrane fusion [58].

(iii) The barrel-stave model typified by PMLA trileucine (PMLA-LLL, H$_{100}$,x) [53]. Trileucine in the side chain of PMLA-LLL, H$_{100}$,x has three hydrophobic isobutyl groups and one α-carboxylic acid end-group that is subject to pH-dependent protonation. At neutral pH, ionized PMLA-LLL, H$_{100}$,x is likely to generate a random-coil conformation, similarly to PMLA, and is largely unable to penetrate the cell membrane owing to its negative charge. As the pH was decreased below 6, PMLA trileucine was found to form aggregates via oligomerization that vertically pierce the membrane core and tentatively form a transmembrane pore to allow entry. In this manner, an increase in the fraction of hydrophobic substituents or the molar mass of the amphiphilic polymer could augment its membranolytic activity [59,60]. Importantly, acidic pH-triggered membranolysis would enable selective disruption of intracellular membranes by ionizable polymeric carriers, including endosomes that are of particular interest for drug delivery (pH ~5.5), thus escaping endosomal capture and lysosomal degradation, leading to release of drug payloads in the cytosol, thereby promoting intracellular drug trafficking and targeting.

In addition to PMLA conjugation with hydrophobic ligands through covalent coupling, methods to regulate its membrane permeability have been developed by promoting non-covalent interactions between the pendant carboxylic acids of PMLA and attaching moieties to the polymer. Given that protonated PMLA can only form hydrogen bonds with functional groups containing electronegative atoms at acidic pH [44], and these are much weaker than covalent or ionic bonds, PMLA

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**Box 2. Hydrophilic–Hydrophobic Balance of PMLAs**

In view of its hydrophilicity and negative charge at physiological pH, PMLA is a polyanion that has little affinity for negatively charged lipid bilayers and does not translocate through cell membranes. To increase the interaction between the biopolymer and the plasma membrane, methylation of carboxylic acid groups with different levels of diazomethane was used to generate a PMLA-Me,H$_{100}$,x copolymer (where x is the percentage of methyl units) [77,78]. As x increases, the hydrophobicity of the molecule increases in the order PMLA < PMLA-Me,H$_{100}$ < PMLA-Me,H$_{50}$ < PMLA-Me,H$_{25}$ < PMLA-Me. Both PMLA-Me,H$_{100}$ and PMLA-Me were completely insoluble in water, similarly to PMLA benzyl esterification. The same order was observed for hydrolysis in saline and plasma, rupture of liposome membranes, and cytotoxicity [77]. In addition, hydrophobic amino acids or peptides can be conjugated to PMLA side-chain carboxylic acids to modulate its hydrophilicity and net charge, thus tuning the interplay with cellular/subcellular membranes in a pH-responsive manner. Adjacent carboxylic acid pendant on the PMLA backbone are five atoms apart, equal to their distance in poly(aspartic acid) that has a similar membranolytic profile [79]. Importantly, this spacing dictates an optimized combination of physicochemical parameters for side-chain substituents, including their individual hydrophobicity, charge-neutralizing capacity, ligand length, and density, thus determining the optimal molecular geometry and charge distribution for effective membrane disruption [79,80].
complexes generated by hydrogen bonding are unsuitable for membranolytic modification or pharmaceutical loading. Nonetheless, the generation of PMLA ionic complexes via electrostatic interactions offers an alternative strategy for enhanced cellular uptake. At neutral pH, PMLA is a polyanion in which negatively charged carboxylates can form stable complexes with positively charged compounds [61]. Depending on the stoichiometry and chemistry of the attached cations, the polyelectrolyte complexes generated can have a variety of sizes, surface charges, water solubilities, molecular structures, and morphologies, each modulating their membrane penetration. In a scenario where anionic PMLA segments are preferentially situated on the surface of polyelectrolyte complexes, they are internalized via non-specific endocytosis. Conversely, cationized PMLA complexes translocate into cells in a similar manner to polycations, which adsorb onto the hydrophilic outer surface of the cell membrane and then induce the formation of aqueous pores or defects in the membrane hydrophobic core, and subsequently integrate into or permeabilize the cell membrane [62]. Once transported into the cytoplasm, pH reduction or, to a lesser extent an increase in ionic strength, would accelerate hydrolytic degradation of the PMLA backbone and dissociation of ionic bonds, liberating the complexed moiety for intracellular utility [61].

**PMLA as a Nanosized Platform for Cancer Diagnosis and Therapy**

A novel type of PMLA-based nanoconjugate has been developed, termed Polycelfin [63]. Through step-by-step chemical synthesis, PMLA was activated by N-hydroxysuccinimidyl ester to enable direct conjugation or further modification by linker molecules, permitting linkage with a variety of chemical and biological ligands, including polyethylene glycol (PEG), monoclonal antibody against transferrin receptor (TfR), an endosome escape unit (LLL or LOEt), and two antisense oligonucleotides (AONs) [64], to synergistically inhibit the 4 and 1 chains of laminin-8 that are overexpressed by human glioblastoma (glioblastoma multiforme, GBM); a fluorescent reporter was also covalently bonded with the PMLA backbone to visualize and localize the biodistribution of Polycelfin (Figure 4) [63]. The attachment of pendant functionality groups established a new hydrophobic–hydrophilic balance (Box 2) in the macromolecular structure, as the sizes of pure PMLA and variant Polycelfins were determined to be <10 and ~20 nm, respectively [65]. These PMLA-based nanoconjugates provide a multifunctional delivery system that can effectively pass through the blood-brain and blood–tumor barriers, leading to enhanced accumulation in brain tumors following i.v. injection into the mouse tail, thus allowing visualization of cancerous lesions and liberating medicinal agents to inhibit tumor angiogenesis or growth [15].

Since this invention, variant Polycelfin biopolymers have been made by combining them with different therapeutic antibodies [66,67], penetrating peptides [5,68], and fluorescent or magnetic contrast agents [69–71] that are linked to the PMLA chain through direct or indirect conjugation chemistry, and these have demonstrated improved targeting and accumulation in specific tumors such as breast and brain cancers. Notably, by targeting and inhibiting the laminin α4 and β1 subunits, treatment of mice bearing intracranial human GBM xenografts with PMLA nanoconjugates led to significantly prolonged survival and reduced tumor sizes relative to mice bearing GBMs in which laminins had been knocked out using CRISPR/Cas9 [10]. The minute physical size, potential for multifunctional conjugation, and outstanding water solubility of these PMLA conjugates give them enormous advantages over many other drug delivery systems in terms of finding their way through a labyrinth of cancers, highlighting their huge potential for clinical translation.

**Concluding Remarks**

Microbial production of PMLA currently remains a challenge because of its low yield, high cost, and the difficulty in defining the length of the biopolymer produced (see Outstanding Questions). Novel gene-editing techniques are urgently needed that would allow efficient delivery of
exogenous gene sequences into *Physarum* plasmodia or filament fungal cells to upregulate PMLA production. CRISPR/Cas9-mediated gene modification was recently successfully applied in *A. pullulan*, leading to a mutation rate nearly ten-fold higher than that obtained by traditional homologous recombination [72]. It is likely that further genes involved in PMLA biopolymerization will soon be identified, with the prospect of producing PMLA in a controlled manner by using novel gene-editing tools that preselect high-yielding strains. Indeed, PMLA per se could be used as an effective transmembrane gene-delivery shuttle. Future genetic modifications will be necessary not only to increase PMLA yield but also to predetermine the molecular weight of the polymer. Furthermore, suppression of polymalatase to inhibit the decomposition of PMLA could also be achieved through gene editing, thus increasing control over both polymer yield and length. Therefore, to harness the potential of biopolymer production, further elucidation of the genes and molecular machinery that mediate the biosynthesis of PMLA and its decomposition will be essential.

Figure 4. Poly(β-L-Malic Acid) (PMLA)-Based Nanoconjugates for Brain Tumor Imaging and Therapy. (A) Scheme and chemical formula of Polycin, attached to (from left to right) an endosome escape unit (LLL or LOEt), AONs to laminin-411 α4 and β1 chains with disulfide linkages cleavable by glutathione, capped unused sulfhydryls, mAb (Ms) targeting the blood–tumor barrier (BTB) endothelium (mouse TfR), mAb (Hu) targeting tumor cells (human TfR), tracking dye Alexa fluor 680, pendant carboxylates for water solubility. (B) Viability of human U87MG glioma cells treated with PMLA conjugates containing pH-dependent (LLL, i.e., P/LLL) or pH-independent (LOEt, i.e., P/LOEt) endosome escape units for 24 h. Cells treated with P/LOEt (not P/LLL) showed low viability at high concentrations, and their early apoptosis could be visualized by microscopy (20× magnification) and examined by FACS analysis after double staining with propidium iodide and FITC-labeled annexin V. (C) Western blot analysis showing inhibition of laminin-411 α4 and β1 chain synthesis in human U87MG glioma cells after treatment with PBS, AON, P/AON/Hu, P/LOEt/AON/Hu, and P/LLL/AON/Hu, where P/LLL/AON/Hu was the most effective. (D) U87MG cells (10^5) were implanted intracranially in mice 21 days before they were treated with different PMLA nanoconjugates for 24 h after intravenous (i.v.) injection, namely P/LLL/AON/Ms (Ms, anti-mouse TfR), P/LLL/AON/Hu (Hu, anti-human TfR), P/LLL/AON/Hu/Ms, P/LOEt/AON/Hu/Ms, and P/LLL/AON/γG (unrelated IgG), all labeled with Alexa fluor 680 to visualize tumor accumulation. The PMLA nanoconjugate with both Ms and Hu mAbs showed the highest tumor accumulation, whereas LLL ensured higher drug tumor accumulation than LOEt, and a control with an unrelated IgG showed low accumulation. Abbreviations: AON, antisense oligonucleotide; FACS, fluorescence-activated cell sorting; FITC, fluorescein isothiocyanate; Hu, human (mAb); LLL, trileucine; LOEt, leucine ethyl ester; mAb, monoclonal antibody; Ms, mouse (mAb); P, PMLA moiety; PBS, phosphate-buffered saline; PEG, polyethylene glycol; TfR, transferrin receptor. Figure reproduced, with permission, from [65].
Because PMLAs represent a versatile platform for both disease diagnosis and treatment, further research is required into the PMLA biosynthetic machinery, the biosafety of bioproduced PMLA, and clinical translation of PMLA for the detection and therapy of diseases (particularly at early stage) including cancers. There is also an urgent need to scale-up PMLA production from the laboratory to the industrial pilot plant. In addition, multiple new uses of biodegradable PMLA in daily life can be envisaged, and this would not only stimulate industrial interest in PMLA bioproduction and increase the popularity of PMLA as a natural biomaterial, but would also promote wider medical applications of these remarkable biopolymers.

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