Research Article

Effects of Puerarin Combined with PLGA/TCP/Puerarin on Osteocalcin and Sialoprotein of Mandibular Defects

Ying Guo,¹,² Qianqian Zhang,¹,² Nu Mi,³ Chunmei Li,⁴ Xuechao Lv,⁵ and Hong Wang ¹,²

¹Department of Stomatology, Shenzhen University General Hospital, Shenzhen 518055, China
²Institute of Stomatological Research, Shenzhen University, Shenzhen 518055, China
³Department of Stomatology, Shenzhen OCT Hospital, Shenzhen 518000, China
⁴Department of Outpatient Stomatology, Heilongjiang Provincial Hospital, Harbin 150000, China
⁵Department of Pediatric Dentistry, The First Affiliated Hospital of Harbin Medical University, Harbin 150000, China

Correspondence should be addressed to Hong Wang; wangham@szu.edu.cn

Received 22 June 2022; Revised 19 July 2022; Accepted 2 August 2022; Published 6 September 2022

Academic Editor: Yuvaraja Teekaraman

In order to evaluate the effects of puerarin combined with poly lactic-co-glycolic acid (PLGA)/tricalcium phosphate (TCP)/puerarin on osteocalcin and sialoprotein of mandibular defects, the obtained rat jaw cells are analyzed. The surface morphology of osteoblast complex in the scaffold material group and puerarin combined scaffold material group is observed by a scanning electron microscope, and the growth and proliferation of osteoblasts are detected by the Cell Counting Kit-8 (CCK-8) method. Besides, the expression of type-I collagen (COL-I), osteocalcin (OC), and osteopontin (OPN) mRNA and related proteins in osteoblasts are detected by immunocytochemical staining. The results of immunocytochemical staining show that puerarin and PLGA/TCP/ puerarin scaffold had significant effects on the expression of COL-I and OC mRNA and related proteins in osteoblasts. The experimental results indicate that puerarin and PLGA/TCP/puerarin can synergistically affect the mRNA and protein expressions of COL-I, OC, and OPN in osteoblasts and have a positive effect on promoting the proliferation activity of osteoblasts.

1. Introduction

Periodontitis is a chronic bacterial infectious disease that occurs in periodontal supporting tissue. Periodontitis causes tooth loosening and falling off, which seriously affects patients’ oral health [1]. Periodontal pathogens not only cause direct damage to periodontal tissue through bacteria themselves and their toxic metabolites but also cause serious damage to the body through long-term persistent inflammation and immune response caused by bacteria [2]. As one of the common clinical problems in stomatology, periodontitis leads to alveolar bone absorption and jaw defects, which seriously affect the beauty, chewing, and pronunciation of patients [3]. The classic method of clinical treatment of alveolar bone and jaw defects is to use appropriate bone filling materials to fill the defect site, so as to enhance the ability of defect repair. At present, bone tissue engineering technology provides a good prospect for the reconstruction of personalized and functional bone defects in the repair of jaw defects. However, there are still many deficiencies in biomaterials [4]. The emergence of 3D printing technology provides a new solution [5]. It realizes the construction of bioactive scaffolds to promote the bone through the function-oriented design of bone repair material structure and the manufacture of fine bionic structures with appropriate mechanical strength [6, 7]. It is also a hot topic of joint exploration in clinical oral and maxillary and biomaterial fields in recent years. In this study, the periodontitis model is established in rat maxillary molars and the jaw defect model is established in the mandibular body. A low-temperature 3D printing technology is used to combine the clinical drug puerarin into degradable polymer and bioceramic materials, and degradable porous drug-containing scaffold materials can be obtained eventually. To realize the effective repair of
the inflammatory alveolar bone defect, the precise control of the molding process, good biocompatibility, appropriate mechanical properties, controllable microporous structure, controllable degradation rate, and the growth rate of new bone roughly should be collaborated synchronously.

The rest of the study is organized as follows: Section 2 discusses related studies, and Section 3 introduces the experimental materials and proposed methods. Section 4 describes the comparative results and analysis chiefly. Section 5 provides the summary.

2. Related Works

Maxillofacial trauma, inflammation, tumors, and other diseases can cause jaw defects, which often lead to facial deformities and masticatory dysfunction [8]. However, the complex shape and function of the jaw is a major challenge for maxillofacial surgery [9]. With the continuous development of immunology, material science, cell biology, and tissue engineering, new materials, new technologies, and new methods emerge in endlessly. The rise of tissue engineering provides more theoretical guidance and technical support for the treatment of jaw defects. Osteoblasts and biological scaffold materials are important elements in bone tissue engineering [10, 11].

The participation of cells is very important in tissue engineering bone construction. In the case of a large bone tissue defect, if there are not enough osteoblasts around the bone repair material, the bone cannot be formed [12]. If cavity-type bone defects, the wound surface is lined with a large amount of blood and tissue fluid, containing a large number of undifferentiated mesenchymal cells. There are also a large number of osteoblast precursors on the wound surface of the bone, and these cells with osteogenic potential can enter the gap of the repair material and fill the whole bone repair area and then proliferate and differentiate into the new bone under the biological induction of the material [13, 14]. The PLGA/TCP/puerarin scaffolds can overcome not only the defects of biocompatibility, biodegradability, and bone tissue engineering orientation of previous materials but also have the characteristics of other materials that are difficult to solve the category of osteogenic activity with existing theories. To screen the gene spectrum and express the induction factor required for tissue formation, for instance, the ideal proportion combination of a variety of inorganic active components in the material can be used. [15]. The specific surface area is large, and there are numerous nanopores that are beneficial to cell proliferation and formation of new tissues. It has significant gene regulation effects on calcifying elements such as osteocalcin and alkaline phosphatase [16]. It has a compound three-dimensional structure with a specific proportion of inorganic active elements and a porosity of over 90%, which enables it to adhere to and accommodate osteoblasts and chondrocytes and microvascular and regulate osteoblasts, thereby releasing bone growth factors and inorganic elements in a specific proportion. At the same time, inorganic elements released during the degradation of scaffold materials can provide nutritional channels necessary for the survival of living cells by neutralizing the acid decomposition products of polylactic acid with its weak alkalinity. Large bone tissue defects can be repaired quickly and effectively by a biological combination of direct central mineralization and osteogenesis [17].

As an isoflavone compound, puerarin has the effects of slowing down heart rate, dilating blood vessels, and lowering blood pressure. It is mainly used in the treatment of hypertension, angina pectoris, cerebral insufficiency, and cerebral infarction [18, 19]. Due to the preventive effect on osteoporosis, extensive attention of researchers has been attracted recently. Some studies have found that puerarin can promote the proliferation and differentiation of osteoblasts, improve alkaline phosphatase activity, and have a good stimulating effect on alkaline phosphatase activity through in vitro culture of human osteoblasts, which may indicate that puerarin has the function of improving osteoblast bone formation [20, 21]. Scanning electron microscope observation showed that puerarin extended osteoblasts well on PLGA/TCP/puerarin repair scaffold, could be connected into sheets, cell matrix secretion is normal, cells and cell matrix could cover the surface of the material, and had good biological compatibility. PLGA/TCP/puerarin repaired scaffolds can also promote the rapid proliferation of osteoblasts.

Type-I collagen (COL-I), osteocalcin (OC), and osteopontin (OPN) are important osteogenic factors and markers of osteoblast differentiation. Col-I, specific collagen secreted by osteoblasts, is the main bone structural protein, providing a scaffold for calcium salt deposition and cell adhesion and can be used as an indicator to evaluate the functional status of osteoblasts [22]. OC is a kind of noncollagenous protein specifically secreted by osteoblasts, which is a marker of osteoblast mineralization to the matrix and can reflect osteoblast activity. OPN is also one of the markers of osteoblasts [23]. OPN promotes the absorption and mineralization of the bone matrix and plays an important role in the process of bone formation and remodeling. In this study, mRNA and protein expressions of osteogenic factors COL-I, OC, and OPN in osteoblasts are detected by RT-PCR and immunocytochemical staining. COL-I, OC, and OPN proteins are all expressed in the cytoplasm of osteoblasts, and the positive reaction is brownish yellow granules. Factorial variance analysis shows that puerarin and porous tantalum scaffolded can synergistically promote the expression of COL-I and OC in osteoblasts. However, it has no significant effect on the expression of OPN. Previous studies have found that puerarin and estradiol can increase the expression of BSP and OCmRNA. Puerarin and estradiol can reduce the expression of OPNmRNA, suggesting that puerarin can promote osteoblast differentiation by affecting the mRNA expression of characteristic proteins related to osteoblast differentiation [24]. Other studies found that puerarin significantly increased ALP activity and COL-I secretion within 0.01–1 μmol/L in a dose-dependent manner to promote differentiation and maturation of human osteoblasts [25].
3. Experimental Materials and Proposed Methods

3.1. Study Objects. 3-4-week-old female SD rats, SPF grade, were supplied by Shanghai Slack Experimental Animal Center; the primers for OPG, RANKL, Runx2, OPN, OC, and GAPDH are synthesized by Shanghai Shenggong Bio-engineering Co., Ltd. Gegensu is purchased from Shanghai Hengfei Biotechnology Co., Ltd. (Art. P9050); DMEM high sugar medium is purchased from Shanghai Microscience Biotechnology Co., Ltd. (Art. L0104-100). SDS-PAGE gel preparation kits (LPS, FBS, PBS buffer, Trypsin-EDTA digestive solution, 100× penicillin-streptomycin mixture) are purchased from Solarbio, Inc. ((Art. L8880, 11011–8611, P1022, T1300, P1400, P1200-) 50 t); osteogenesis induction medium is purchased from Baizhi Biomedical Technology (Shanghai) Co., Ltd. (Biosmedi-D5-8001). RNAlso Plus, reverse transcription kit, and fluorescence quantitative PCR kit are purchased from Takara Company in Japan (article number: RR037Q/A/B, 639519). Alkaline phosphatase detection kit, RIPA lysate, and BCA kit are purchased from Shanghai Biyuntian Company (article number: P0321, P0013 K, P0011). 3900 high throughput DNA synthesizer is purchased from Applied Biological Systems, Inc. CFX96 Touch Deep Well Fluorescent quantitative PCR instrument is purchased from Bio-Rad Company, USA. Elx800 microplate meter, 1659001 protein electrophoresis meter, and Trans-Blot SD semidy membrane transfer instrument are purchased from Bio-Rad Company in the United States. The Cxk41-f32f optical microscope is purchased from Olympus Company, Japan. Centrifuge 5424R low-temperature high-speed centrifuge is purchased from Eppendorf GMBH in Germany.

3.2. Main Reagents and Instruments

3.2.1. Isolation and Culture of Rat Jaw BMSCs. The female SD rats aged 3-4 weeks are sacrificed by neck dissection and immersed in 75% ethanol solution for 5 min. The mandible and bilateral iliac bones are removed, respectively, in a sterile environment, the attached soft tissues are removed, and sterile PBS is repeatedly rinsed. Next, the bone marrow puncture needle 21# is used to pierce 4-5 holes in the bone cortex, and the cells are repeatedly rinsed with α-MEM. The collected cell suspensions are placed in Petri dishes and cultured at 5% CO₂ and 37°C. After 48h of culture, BMSCs are first half-changed and then the fresh medium is replaced every 3 days. The proliferation number and growth status of stem cells are observed by an inverted phase contrast microscope. The third-generation BMSCs can be used for the experiment.

3.2.2. Preparation of Complete Medium. Add 10% fetal bovine serum and 100 U/mL penicillin-streptomycin into DMEM high-glucose medium and mix them upside down. The purchased frozen cell lines are thawed in a waterbath at 39°C for 30 minutes, centrifuged at room temperature for 5 min, suspended in a complete medium, mixed, and cultured in a cell incubator with 5% carbon dioxide at 37°C. When the cells grew to about 85%, the cells are digested with trypsin and subcultured in a 96-well plate at a ratio of 1:3. Mc3t3-e1 cells are divided into the control group, model group, and puerarin group by the random number table method. Mc3t3-e1 cells are treated with 1 μg/mL LPS for 24h. The puerarin group cells are treated with 10 nmol/L puerarin (dissolved in DMEM high sugar medium) and cultured for 24h. Cells of each group are collected on three plates for reserve, and the cell culture medium of each group is collected on the other plate. After being rinsed by PBS, cells are fixed with 4% paraformaldehyde solution for reserve.

3.2.3. Cells Are Cocultured with Puerarin Combined with PLGA/TCP/Puerarin Scaffold Material. PLGA/TCP/puerarin scaffold material is cleaned with ultrasonic cleaner for 15 min and autoclaved for 30 min. It is then kept into a sterile 6-well plate, α-MEM medium prewet, and 24h later, the excess liquid is discarded and set aside. 300 μL 1 μmol/L drug-treated cell suspension with a density of 2×10⁶ cells/mL is inoculated on the surface of scaffold material and incubated at 37°C for 2h in an incubator with 5% CO₂. The scaffold material is turned upside down and the other side of the material is added according to the above inoculation method and incubated at 37°C for 2h in an incubator with 5% CO₂. 2 mL α-MEM medium is added into each well, and the culture is continued.

3.2.4. Experimental Grouping. The scaffold material group is defined as PLGA/TCP/puerarin scaffolds that are cocultured with osteoblasts. Puerarin combined with the scaffold material group is defined as puerarin, PLGA/TCP/puerarin scaffold materials that are cocultured with osteoblasts. Besides, the blank group is defined as osteoblast culture.

3.3. Detection of Osteogenic Differentiation

3.3.1. CCK-8 Method. A 50 μL CCK-8 solution is added, and the 24-well plates are placed in an incubator with 5% CO₂ at 37°C for 2h. Absorb 100 μL supernatant from each well of the 24-well plate and add it successively to each well of the 96-well plate. The absorbance (OD) of each well in the 96-well plate is measured by a microplate reader at 490 nm.

3.3.2. Expression Levels of COL-I, OC, and OPN mRNA Are Detected by RT-PCR. Trizol’s one-step method is used to extract the total RNA from each group of osteoblasts cultured for 5 days. The total RNA concentration and purity are calculated according to the formula, and the RNA concentration is adjusted to 500 ng/μL. CDNA is synthesized using M-MuLV reverse transcriptase, Primer5.0 software is used to design primers, and PCR primer sequences of each gene are synthesized, as shown in Table 1. SYBRqPCRmix is used for PCR amplification system reaction. The PCR amplification system is set to reverse for 5s, annealing at 56°C for 25s, extension at 72°C for 20s, a total of 40 cycles, and
Table 1: Primers of target gene and reference gene.

| Name of the primer | Primer | The sequence (5‘-3′) |
|--------------------|--------|---------------------|
| OC Primer F        |        | CTTGATTGCAAGGACAGCA |
| OC Primer R        |        | GCGGCTTCAGGCTCACAC |
| OPN Primer F       |        | GCTTTGCTTATGGACTGAGG |
| OPN Primer R       |        | GCCATCTTCAAGCCTGAC  |
| COL-1 Primer F     |        | AGTGGTTGATGGTGGCAA  |
| COL-1 Primer R     |        | GCCCATATTTCCACAGGC |
| GAPDH Primer F     |        | AGTCAGGTATCCCACAGGAAACAG |
| GAPDH Primer R     |        | TGTGCAGCGCGTGATCTGA  |

extension at 72°C for 5 min. PCR results are analyzed using Comparative delta-delta Ct.

3.3.3. Expression of COL-I, OC, and OPN Proteins by Immunocytochemical Staining. Each group is prepared into single-cell suspension and inoculated into a 6-well plate with sterile cover glass at a density of 1×10⁶ cells/mL. After the cells grew to semiconglutination, the sterile cover glass is taken out, discarded paraformaldehyde for 30 min, and fixed with 4% paraformaldehyde solution, and ished with PBS 3 times; an appropriate amount of 0.5% Triton-100 is dropped onto the cover glass, and ished with PBS 3 times, 2 min per time. An appropriate amount of formaldehyde for 30 min, discarded paraformaldehyde solution, and ished with PBS 3 times; an appropriate amount of 0.5% Triton-100 is dropped onto the cover glass, which is lysed at room temperature for 20 min, and ished with PBS 3 times, 2 min/time; an appropriate amount of 3% of H₂O₂ is dropped onto the cover glass and incubated at room temperature for 15 min to achieve the effect of blocking endogenous peroxidase, and ished with PBS 3 times and added a proper amount of primary antibody (1:150) overnight at 4°C, ished with PBS 3 times, 2 min/time; an appropriate amount of secondary antibody is dropped and incubated at 37°C for 30 min and then ished 3 times with PBS, 2 min each. DAB is used for color rendering, and the cover glass is immersed in gradient alcohol for step-by-step dehydration. Xylene is transparent, and neutral gum is used for routine sealing. Image-Pro Plus Image analysis software is used for semiquantitative analysis of dyeing index results.

3.4. Observation Indicators. The observation indicators include the following: (1) PLGA/TCP/puerarin scaffold materials and composites are observed under scanning electron microscopy; (2) observe the proliferation of osteoblasts; (3) the mRNA expression levels of COL-I, OC, and OPN in osteoblasts are observed; (4) the expressions of COL-I, OC and OPN proteins in osteoblasts are compared.

3.5. Statistical Treatment. SPSS 26.0 software is used for statistical analysis of the data, and the count data are expressed as rate (%). The mean ± standard deviation of measurement data indicated that one-way ANOVA is performed for comparison between groups, and the LSD t-test is used for further pairwise comparison. P < 0.05 is considered statistically significant.

4. Comparative Results and Analysis

4.1. Scaffold Materials and Composites under Scanning Electron Microscopy. The PLGA/TCP/puerarin scaffold material under scanning electron microscopy has a large number of uniformly dispersed microporous structures with diameters of about 400~600 μm. The internal pores are interconnected, and the interpore trabecular pillars are microporous. Under scanning electron microscopy, osteoblasts are observed on the surface of the scaffold material and in the micropores to form layers of adhesion and growth, extending out cell pseudopodia, connecting with each other, and fusing into sheets, and secreted matrix covered the surface of the scaffold and in the micropores. The results showed that osteoblasts had good extensibility on the scaffold and could be connected into sheets. The secretion of the cell-matrix is normal, and cells and cell matrix could cover the surface of the scaffold material, as shown in Figure 1.

4.2. Observation of the Proliferation of Osteoblasts. OD values of each group are measured at 1 d, 3 d, 5 d, and 7 d by ELISA. The results indicate that the proliferation activity of puerarin combined with the scaffold material group increased significantly than that of the blank group with the time extension, with a statistical significance (P < 0.05). The proliferation activity of the scaffold material group increases significantly than that of the blank group (P < 0.05), as shown in Table 2. The symbol “*” represents P < 0.05 compared with the blank group.

4.3. Comparison of the mRNA Expression Levels of COL-I, OC, and OPN in Osteoblasts. In this experiment, the CT method is used to analyze and process the data, and it is shown that the mRNA expression levels of COL-I and OC in puerarin combined with the scaffold material group and scaffold material group increased significantly than those in the blank group (P < 0.05), and the mRNA expression levels of COL-I and OC in puerarin combined with the scaffold material group increased significantly than those in other groups. There is no significant difference in the expression of OPN mRNA among all groups (P > 0.05). After one-factor analysis of variance, puerarin and PLGA/TCP/puerarin scaffold materials can promote the high expression trend of COL-I and OC mRNA in osteocytes. The expression of COL-I and OC mRNA is synergistically promoted, but OPN mRNA is not significantly affected, as shown in Table 3. The symbol “#” represents P < 0.05 compared with the stent material group.

4.4. Expressions of COL-I, OC, and OPN Proteins in Osteoblasts. Analysis of osteoblasts in each group by immunocytochemical staining showed that COL-I, OC, and OPN proteins are all expressed in the cytoplasm of osteoblasts, and the positive reaction is brownish yellow granules, indicating that COL-I, OC, and OPN are expressed in osteoblasts and the positive reaction is brownish yellow granules, indicating that COL-I, OC, and OPN are expressed in osteoblasts.
those in the blank group ($P < 0.05$), and the expressions of COL-I and OC in the puerarin combined with the scaffold group are significantly higher than those in the other groups ($P < 0.05$), but the comparison of OPN protein expression among all groups is $P > 0.05$. The results of one-way variance analysis show that puerarin and PLGA/TCP/ruerarin scaffold materials can promote the expression of COL-I and OC proteins. They have a synergistic effect on the expression of these proteins.

**Table 2: Comparison of osteoblast proliferation (OD).**

| Group                                    | 1d          | 3d          | 5d          | 7d          |
|------------------------------------------|-------------|-------------|-------------|-------------|
| The blank group                          | $0.163 \pm 0.035$ | $0.425 \pm 0.038$ | $1.133 \pm 0.047$ | $1.351 \pm 0.073$ |
| Bracket material group                   | $0.177 \pm 0.028^*$ | $0.647 \pm 0.031^*$ | $1.161 \pm 0.036^*$ | $1.552 \pm 0.051^*$ |
| Puerarin combined with the scaffold material group | $0.179 \pm 0.016^*$ | $0.752 \pm 0.046^*$ | $1.184 \pm 0.041^*$ | $1.771 \pm 0.046^*$ |
| $F$                                      | 1.134       | 4.276       | 4.023       | 5.117       |
| $P$                                      | 0.112       | <0.001      | <0.001      | <0.001      |

**Table 3: Comparison of mRNA expression of COL-I, OC, and OPN in osteoblasts.**

| Group                                    | COL-I       | OC          | OPN         |
|------------------------------------------|-------------|-------------|-------------|
| The blank group ($n = 3$)                | 1.00        | 1.00        | 1.00        |
| Bracket material group ($n = 3$)         | $1.45 \pm 0.55$ | $1.55 \pm 0.25$ | $1.08 \pm 0.31$ |
| Puerarin combined with the scaffold material group ($n = 3$) | $1.96 \pm 0.27^*$ | $1.84 \pm 0.59$ | $1.14 \pm 0.53$ |
| $F$                                      | 8.227       | 8.695       | 2.034       |
| $P$                                      | <0.001      | <0.001      | 0.116       |

**Table 4: Comparison of COL-I, OC, and OPN protein expression detected by immunocytochemical staining.**

| Group                                    | COL-I       | OC          | OPN         |
|------------------------------------------|-------------|-------------|-------------|
| The blank group ($n = 9$)                | $14.167 \pm 0.525$ | $16.215 \pm 1.037$ | $15.887 \pm 0.664$ |
| Bracket material group ($n = 9$)         | $16.785 \pm 0.872$ | $17.526 \pm 1.121$ | $16.262 \pm 1.427$ |
| Puerarin combined with the scaffold material group ($n = 9$) | $18.221 \pm 0.514$ | $19.117 \pm 1.134$ | $16.354 \pm 0.421$ |
| $F$                                      | 7.546       | 8.014       | 1.817       |
| $P$                                      | <0.001      | <0.001      | 0.235       |
of COL-I and OC proteins but cause no significant effect on the expression of OPN protein, as shown in Table 4.

5. Conclusions

In this study, the effects of puerarin PLGA/TCP/puerarin repair scaffold on the expression and cell proliferation of osteoblast osteogenic factors COL-I, OC, and OPN are investigated. The experimental result can provide a scientific theoretical basis for puerarin and PLGA/TCP/puerarin repair scaffold materials for the treatment of bone defects and fracture healing. In addition, the medicinal value and clinical trial range of puerarin will be expanded based on the inherent clinical treatment of osteoporosis. The findings can improve the application scope of *Pueraria lobata* and play an important role in mining the medicinal value and economic value of *Pueraria lobata*. Isomorphism is an active attempt and exploration of the molecular biology experiment of traditional Chinese medicine. It can also bring positive exploration and attempt to the treatment of bone repair with integrated traditional Chinese and Western medicine. In future work, we will further explore the clinical effect of puerarin as an auxiliary drug for bone graft scaffold material to repair bone defects in promoting bone growth, so as to provide a theoretical and practical basis for further clinical application.

Data Availability

The data used to support the findings of this study are available from the corresponding author upon request.

Conflicts of Interest

The authors declare that they have no conflicts of interest.

Authors’ Contributions

Chunmei Li contributed equally to the first author.

Acknowledgments

The work was supported by Guangdong Scientific Research Foundation (A2021297) and Natural Science Foundation of Shenzhen University General Hospital (SUGH2020QD016).

References

[1] L. Guo, K. Li, J. Zhou, and L. Luo, “Panax notoginseng saponin Rg1 can effectively improve the cognitive function of 5×FAD mice,” *Journal of Healthcare Engineering*, vol. 2022, no. 7, 26 pages, Article ID 5132761, 2022.

[2] W. J. Kim, S. Y. Park, and O. S. Kim, “Autophagy upregulates inflammatory cytokines in gingival tissue of patient with periodontitis and lipopolysaccharide-stimulated human gingival fibroblasts,” *Journal of Periodontology*, vol. 3, no. 7, pp. 19–22, 2021.

[3] R. Zhou, L. Shen, C. Yang et al., “Periodontitis may restrain the mandibular bone healing via disturbing osteogenic and osteoclastic balance,” *Inflammation*, vol. 41, no. 3, pp. 972–983, 2018.

[4] D. G. Boeckel, P. Sesterheim, T. R. Peres et al., “Adipogenic mesenchymal stem cells and hyaluronic acid as a cellular compound for bone tissue engineering,” *Journal of Craniofacial Surgery*, vol. 30, no. 3, pp. 777–783, 2019.

[5] W. F. Yang, L. Long, R. Wang, D. Chen, S. Duan, and F. J. Xu, “Surface-Modified hydroxyapatite nanoparticle-reinforced polyactides for three-dimensional printed bone tissue engineering scaffolds,” *Journal of Biomedical Nanotechnology*, vol. 14, no. 2, pp. 294–303, 2018.

[6] M. Ge, K. Ge, F. Gao et al., “Biomimetic mineralized strontium-doped hydroxyapatite on porous poly (L-lactic acid) scaffolds for bone defect repair,” *International Journal of Nanomedicine*, vol. 13, no. 5, pp. 1707–1721, 2018.

[7] K. Kiho, S. Sumitomo, M. Tanaka et al., “Pulpal disease arising from medication-related osteonecrosis of the jaw: a case report,” *Journal of Endodontics*, vol. 46, no. 8, pp. 1149–1154, 2020.

[8] E. J. Castillo, J. G. Messer, A. M. Abraham et al., “Preventing or controlling periodontitis reduces the occurrence of osteonecrosis of the jaw (ONJ) in rice rats (Oryzomys palustris),” *Bone*, vol. 145, Article ID 115866, 2021.

[9] J. I. Aguirre, E. J. Castillo, and D. B. Kimmel, “Biologic and pathologic aspects of osteocytes in the setting of medication-related osteonecrosis of the jaw (MRONJ),” *Bone*, vol. 153, Article ID 116168, 2021.

[10] S. Okuma, Y. Matsuda, Y. Nariai, M. Karino, R. Suzuki, and T. Kanno, “A retrospective observational study of risk factors for denosumab-related osteonecrosis of the jaw in patients with bone metastases from solid cancers,” *Cancers*, vol. 12, no. 5, pp. 1209–1217, 2020.

[11] G. Ascone, Y. Cao, I. D. Jansen et al., “Increase in the number of bone marrow osteoclast precursors at different skeletal sites, particularly in long bone and jaw marrow in mice lacking IL-1RA,” *International Journal of Molecular Sciences*, vol. 21, no. 11, pp. 3774–3778, 2020.

[12] S. Behjat, M. Rybachuk, and Y. G. Anissimow, “Electrosprun PGs/PCL, PLLA/PCL, PLGA/PCL and pure PCL scaffolds for retinal progenitor cell cultivation,” *Biochemical Engineering Journal*, vol. 4, no. 6, pp. 166–173, 2020.

[13] F. Figeac, M. Tencerova, D. Ali et al., “Impaired bone fracture healing in type 2 diabetes is caused by defective functions of skeletal progenitor cells,” *Stem Cells*, vol. 40, no. 2, pp. 149–164, 2022.

[14] Y. K. Yu, Y. Wang, W. D. Zhang et al., “Biomimetic periosteum–bone substitute composed of preosteoblast-derived matrix and hydrogel for large segmental bone defect repair,” *Acta Biomaterialia*, vol. 113, no. 5, pp. 317–327, 2020.

[15] P. Wei, Y. Xu, H. Zhang, and L. Wang, “Continued sustained insulin-releasing PLGA nanoparticles modified 3D-Printed PCL composite scaffolds for osteochondral repair,” *Chemical Engineering Journal*, vol. 422, no. 11, Article ID 130051, 2021.

[16] A. O. Pereira, J. M. I. Lopes, T. R. Silva et al., “Bacterial photoactivation using PLGA electrospun scaffolds,” *ACS Applied Materials & Interfaces*, vol. 13, no. 27, pp. 31406–31417, 2021.

[17] Y. Zhou, H. Lian, K. Liu, D. Wang, X. Xiu, and Z. Sun, “Puerarin improves graft bone defect through microRNA155-mediated p53/TNFα/STAT1 signaling pathway,” *International Journal of Molecular Medicine*, vol. 46, no. 1, pp. 239–251, 2020.

[18] S. R. Huang, S. S. Jin, B. Xu, and R. P. Wang, “Puerarin alleviates the progression of non-small cell lung cancer by regulating the miR-342/CCND1 axis,” *Neoplasma*, vol. 67, no. 06, pp. 1244–1255, 2021.
[19] W. Li, “Supramolecular nanofiber-reinforced Puerarin hydrogels as drug carriers with synergistic controlled release and antibacterial properties,” Journal of Materials Science, vol. 55, no. 15, pp. 6669–6677, 2020.

[20] S. Wang, W. Heng, X. Wang et al., “Coamorphization combined with complexation enhances dissolution of lurapidone hydrochloride and Puerarin with synchronized release,” International Journal of Pharmaceutics, vol. 588, no. 1, Article ID 119793, 2020.

[21] X. Jiang, W. Chen, H. Su, F. Shen, W. Xiao, and W. Sun, “Puerarin facilitates osteogenesis in steroid-induced necrosis of rabbit femoral head and osteogenesis of steroid-induced osteocytes via miR-34a upregulation,” Cytokine, vol. 143, no. 3, Article ID 155512, 2021.

[22] J. S. Wang, K. E. Tanner, S. Abdulghani, and L. Lidgren, “Indentation testing of a bone defect filled with two different injectable bone substitutes,” Key Engineering Materials, vol. 284-286, no. 6, pp. 89–92, 2005.

[23] A. Aprile, L. Raggi, M. Storto et al., “Inhibition of fibroblast growth factor-23 (FGF-23) as a novel strategy to target bone and hematopoietic stem cell niche defects in beta-thalassemia,” Blood, vol. 136, no. 1, pp. 2–9, 2020.

[24] A. Toyota, R. Shinagawa, M. Mano, K. Tokioka, and N. Suda, “Regeneration in experimental alveolar bone defect using human umbilical cord mesenchymal stem cells,” Cell Transplantation, vol. 30, no. 9703, 1785 pages, Article ID 096368972097539, 2021.

[25] C. T. Cidem, A. Türer, and M. C. Durmular, “The local effect of Puerarin on critical sized calvarial defects: a stereological study,” Journal of Craniofacial Surgery, vol. 28, no. 1, pp. 143–151, 2016.