Cryptophane-Folate Biosensor for $^{129}\text{Xe}$ NMR

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Supporting Information

ABSTRACT: Folate-conjugated cryptophane was developed for targeting cryptophane to membrane-bound folate receptors that are overexpressed in many human cancers. The cryptophane biosensor was synthesized in 20 nonlinear steps, which included functionalization with folate recognition moiety, solubilizing peptide, and Cy3 fluorophore. Hyperpolarized $^{129}\text{Xe}$ NMR studies confirmed xenon binding to the folate-conjugated cryptophane. Cellular internalization of biosensor was monitored by confocal laser scanning microscopy and quantified by flow cytometry. Competitive blocking studies confirmed cryptophane endocytosis through a folate receptor-mediated pathway. Flow cytometry revealed 10-fold higher cellular internalization in KB cancer cells overexpressing folate receptors compared to HT-1080 cells with normal folate receptor expression. The biosensor was determined to be nontoxic in HT-1080 and KB cells by MTT assay at low micromolar concentrations typically used for hyperpolarized $^{129}\text{Xe}$ NMR experiments.

INTRODUCTION

Magnetic resonance imaging (MRI) is a noninvasive medical imaging technique most useful for obtaining high contrast in vivo images of tissues, organs, and bone at high spatial resolution. $^1\text{H}$ MRI is limited by low sensitivity, in part due to high background from endogenous proton signals. In order to increase signal, especially when imaging vascular tissues or analyzing brain perfusion, gadolinium- or iron-oxide-based contrast agents are commonly used. However, early and accurate diagnoses of human disease increasingly rely upon information gleaned from molecular imaging of protein biomarkers or metabolic processes. There are now many examples using PET and SPECT imaging agents with readily detected radioactive nuclei. By comparison, current MRI contrast agents have limited ability to detect proteins or metabolites of low abundance in cells. The goal of making “smart” MRI contrast agents that produce readily measurable signals in response to environmental cues has led to intense investigation of nuclei that can be hyperpolarized (HP) to achieve a majority of unpaired nuclear spins, most commonly $^{13}\text{C}$, $^3\text{He}$, $^{129}\text{Xe}$, and $^{38}\text{Kr}$. Recent applications of HP $^{13}\text{C}$ pyruvate in human and small animal MRI highlight the great potential of hyperpolarization techniques for evaluating metabolites associated with prostate cancer and cardiac dysfunction.

$^{129}\text{Xe}$ is a nontoxic gas with high water solubility (4.2 mM atm$^{-1}$ at 300 K) and unique physical–chemical properties that motivate the development of a new class of versatile MRI contrast agents. Xenon’s significant polarizability contributes to its affinity for void spaces in natural and synthetic materials, as well as chemical-shift sensitivity to its molecular environment. Recent advances in $^{129}\text{Xe}$ hyperpolarization technology make this agent now much more accessible, in liter quantities at near-unity polarization levels. Several HP $^{129}\text{Xe}$ MRI studies imaging the lungs and brain have been published, for both rodents and humans. Our laboratory has developed water-soluble tris(triazole ethylamine) and tris-carboxylate derivatives of cryptophane-A that bind xenon with usefully large association constants, $K_A = 17\,000$-$42\,000\,\text{M}^{-1}$ in buffer at 293 K. Additionally, one tris-carboxylate cryptophane was shown to bind $\text{Xe}$ in human plasma with appreciable affinity, $K_A = 22\,000\,\text{M}^{-1}$ at 310 K. The chemical shift of $^{129}\text{Xe}$-bound cryptophane can be modulated stereoelectronically, e.g., by ruthenating the aromatic rings, varying the size of the cavity, or appending water-solubilizing moieties. We and others have synthesized cryptophane biosensors that are conjugated to various ligands via a hydroxyl or propargyl group. These include biotin-modified cryptophane biosensors for detecting streptavidin, an enzyme-responsive biosensor for matrix metalloproteinase-7 (MMP-7), and a series of benzenesulfonamide-functionalized cryptophane-A derivatives that exhibited isozyme-specific chemical shift changes, upon binding carbonic anhydrases I or II. Another example included a peptide-labeled $^{129}\text{Xe}$ biosensor by Schlundt et al. that produced a 1 ppm downfield shift upon binding to a major histocompatibility complex (MHC) class II protein. The delivery of cryptophanes using cell-penetrating peptides or targeting cell-surface $\alpha,\beta_3$ integrin receptors has also been demonstrated with cancer and normal cell lines. Recent efforts have highlighted the potential for using xenon biosensors in cellular HP $^{129}\text{Xe}$ magnetic resonance spectroscopy and imaging.
Folic acid has been investigated over the past two decades as a means for targeted delivery of payloads to tumor cells. In cells, there are three types of transporters that are responsible for the uptake of folate. These include reduced folate carrier (RFC), proton-coupled high affinity folate transporter, and folate receptor (FR, also known as high affinity folate binding protein). Folate receptors are cell surface glycosylphosphatidylinositol (GPI)-linked membrane glycoproteins with molecular weights ranging from 38 to 45 kDa. RFC is ubiquitously expressed throughout normal adult tissue, but as the name implies, this low affinity folate carrier is specific for the physiological form of reduced folic acid, 5-methyl tetrahydrofolate, which binds RFC with a micromolar dissociation constant. The high affinity FR (Kd ≈ 0.1–1 nM, 1:1 stoichiometry) binds the nonphysiological folic acid as well as 5-methyltetrahydrofolate. FR exhibits narrow tissue distribution, being predominately expressed on the apical surface of polarized epithelial cells and thus not in contact with circulating folate. In humans, FR has 4 different isoforms: α, β, γ, and δ, where α and β are membrane-bound. Among them, FRα is overexpressed in non-mucinous adenocarcinomas of the ovary, cervix, uterus, and ependymal brain tumors. Monopropargyl cryptophane was joined to the folate-conjugated azidopeptide on solid support via Cu(I)-catalyzed [3 + 2] azide–alkyne cycloaddition.

Scheme 1. Five-Step Synthesis of [2-(Trimethylsilyl)ethoxy]-2-N-[2-(trimethylsilyl)-ethoxycarbonyl]folic Acid

Scheme 2. Synthesis of Unlabeled and Cy3-Labeled Biosensors 24 and 25, Respectively
overexpressed in 90% of ovarian carcinomas; and higher levels of expression are generally associated with poorly differentiated and aggressive tumors.\textsuperscript{49,50} It is believed that FR\textsubscript{x} is overexpressed because the fast growth rate of cancer cells requires more folic acid.\textsuperscript{45} FR expression is generally absent from normal tissues except in the choroid plexus, the placenta, and at low levels in lung, thyroid, and kidney. These FRs do not present a problem when using folic acid to target cancer because of localizations inaccessible to circulation; the brain side of the blood-brain barrier (choroid plexus), on the luminal side (lungs and gut), and in the proximal tubule lumen (kidney). FR functions via receptor-mediated endocytosis. FR is largely recycled back to the cell surface. Additionally, folate (kidney). FR functions via receptor-mediated endocytosis. FR is largely recycled back to the cell surface. Additionally, folate





FLUORESCENT FOLATE–CRYTOPHANE CONJUGATE (25). Further steps in biosensor synthesis are shown in Scheme 2. The azidopeptide 22 was synthesized by standard solid-phase synthesis using Fmoc-substituted reagents in 85% yield and consisted of three polyethylene glycol units and lysine-arginine units to help solubilize the cryptophane in water.\textsuperscript{58} 3-Azido propionic acid was prepared according to literature procedures and incorporated as the N-terminal residue.\textsuperscript{59} The cysteine was incorporated in the peptide to enable site-specific fluorescent labeling of the biosensor for cell studies. The azidopeptide was orthogonally deprotected using 4% hydrazine in water and readily coupled to the \(\gamma\)-folate conjugate 7 in dry DMF to yield 23 in 75% yield. In order to monitor the reaction, a portion of the reaction mixture was cleaved from the resin and purified by reverse-phase HPLC. Once product formation was confirmed, 23 (still on solid support) was coupled to monopropargyl cryptophane 21 to give 24 by copper(I)-catalyzed \([3 + 2]\) cycloaddition. Although the yield for 24 was initially low (~20%), it was subsequently improved to approximately 80% by using a large excess of sodium ascorbate (40 equiv) to ensure that copper remained reduced as Cu(0) to catalyze the reaction. The product was cleaved from solid support, purified by reverse-phase HPLC and was determined to be readily soluble in water. To fluorescently label the conjugate 24, the cysteine was deprotected using TCEP and coupled with the maleimide-functionalized Cy3 dye \((\lambda_{ex} = 550 \text{ nm}, \lambda_{em} = 575 \text{ nm})\). 25 was purified by reverse-phase HPLC. Cy3 labeling efficiencies were determined from the ratio of dye absorbance at 550 nm \((\varepsilon_{550} = 150 000 \text{ M}^{-1} \text{ cm}^{-1})\) with a correction factor of 0.05 at \(A_{280}\) to the cryptophane absorbance at 280 nm \((\varepsilon_{280} = 10 000 \text{ M}^{-1} \text{ cm}^{-1})\).\textsuperscript{60} Cy3-labeling yields were only 20–30%, likely a result of steric hindrance from both the bulky cryptophane and folate group appended to the peptide. Removal of excess TCEP using a gel filtration column, prior to Cy3 addition, did not improve the yield.

**Visualization of Cell Delivery by Confocal Microscopy.** In order to determine whether 25 could be selectively delivered to FR\textsuperscript{+} cells, confocal laser scanning microscopy (CLSM) was performed as shown in Figure 1. Human nasopharyngeal epidermoid carcinoma cells (KB) and human cervical carcinoma cells (HeLa) were used as receptor positive cell lines, with KB strongly overexpressing FR\textsuperscript{x} and HeLa moderately expressing FR\textsuperscript{−}. Human fibrosarcoma (HT-1080) was used as a negative control cell line (FR\textsuperscript{−}) because

**RESULTS AND DISCUSSION**

**Synthesis and Characterization of Folate–Cryptophane Conjugate.** The fluorescent, folate–cryptophane conjugate was synthesized in 20 nonlinear steps from four commercially available starting materials. Folate recognition moiety 7 (5 steps, Scheme 1), monopropargyl cryptophane 21 (12 steps), and solubilizing azido-peptide 22 were joined in two steps to form biosensor 24 and finally conjugated with Cy3 dye (1 step) to give the fluorescent biosensor 25 (Scheme 2).

**Synthesis of \(\alpha\)-(2-(Trimethylsilyl)ethoxy)-2-N-(2-(trimethylsilyl)-ethoxycarbonyl) Folic Acid (7).** Folic acid has two carboxylates (\(\alpha\)- and \(\gamma\)-) whose reaction with the peptide sequence via \(\text{N},\text{N}’\text{-dicyclohexylcarbodiimide (DCC)}\) would produce a mixture of \(\alpha\)-folate and \(\gamma\)-folate conjugates. Because only the \(\gamma\)-conjugate is recognized by the FR\textsuperscript{x} receptor, a selectively protected folic acid derivative 7 was synthesized in 5 nonlinear steps in 13% overall yield following established protocols (Scheme 1).\textsuperscript{57} The folate recognition moiety was prepared from two intermediates: the 2-N-teoc-pteroic acid derivative, where teoc is 2-(trimethylsilyl)-ethoxycarbonyl, and the \(\alpha\)-carboxyl-protected glutamic acid.\textsuperscript{57} Folic acid 1 underwent enzymatic hydrolysis with carbaptyeptidase-G to give pteroic acid 2. Carboxylidiumidazole (CDI) and 2-trimethylsilylthanol in dry dimethyl sulfoxide (DMSO) were added to the crude pteroic acid to produce the protected pteroic acid, 1-(2-N-teoc-pteroyl)imidazolide 3 in 62% yield. In order to synthesize the second intermediate, the \(\alpha\)-carboxylate group in N-Boc-1-Glu (OBn)-OH 4 was protected by treating it with CDI and 2-trimethylsilylthanol while the \(\gamma\)-carboxylate group was selectively deprotected using Pd–C to give 5 in 88% yield. The N-Boc protecting group was subsequently removed using TsOH to give \(\alpha\)-(2-TMS-ethyl) glutamate 6 in 51% yield. Finally, 3 was treated with 1.5 equiv of 6 and N-methyl-1,5,9-triazabicyclo[4.4.0]-decene (MTBD) in dry DMSO to give the folate recognition moiety 7 (41% yield).

**Monopropargyl Cryptophane (21).** A monopropargyl derivative of cryptophane-A was synthesized in 12 nonlinear steps in 3% overall yield (Supporting Information, Schemes S1–S3).\textsuperscript{35}

**Synthesis and Characterization of Folate–Cryptophane Conjugate (25).** Final steps in biosensor synthesis are shown in Scheme 2. The azidopeptide 22 was synthesized by standard solid-phase synthesis using Fmoc-substituted reagents in 85% yield and consisted of three polyethylene glycol units and lysine-arginine units to help solubilize the cryptophane in water.\textsuperscript{58} 3-Azido propionic acid was prepared according to literature procedures and incorporated as the N-terminal residue.\textsuperscript{59} The cysteine was incorporated in the peptide to enable site-specific fluorescent labeling of the biosensor for cell studies. The azidopeptide was orthogonally deprotected using 4% hydrazine in water and readily coupled to the \(\gamma\)-folate conjugate 7 in dry DMF to yield 23 in 75% yield. In order to monitor the reaction, a portion of the reaction mixture was cleaved from the resin and purified by reverse-phase HPLC. Once product formation was confirmed, 23 (still on solid support) was coupled to monopropargyl cryptophane 21 to give 24 by copper(I)-catalyzed \([3 + 2]\) cycloaddition. Although the yield for 24 was initially low (~20%), it was subsequently improved to approximately 80% by using a large excess of sodium ascorbate (40 equiv) to ensure that copper remained reduced as Cu(0) to catalyze the reaction. The product was cleaved from solid support, purified by reverse-phase HPLC and was determined to be readily soluble in water. To fluorescently label the conjugate 24, the cysteine was deprotected using TCEP and coupled with the maleimide-functionalized Cy3 dye \((\lambda_{ex} = 550 \text{ nm}, \lambda_{em} = 575 \text{ nm})\). 25 was purified by reverse-phase HPLC. Cy3 labeling efficiencies were determined from the ratio of dye absorbance at 550 nm \((\varepsilon_{550} = 150 000 \text{ M}^{-1} \text{ cm}^{-1})\) with a correction factor of 0.05 at \(A_{280}\) to the cryptophane absorbance at 280 nm \((\varepsilon_{280} = 10 000 \text{ M}^{-1} \text{ cm}^{-1})\).\textsuperscript{60} Cy3-labeling yields were only 20–30%, likely a result of steric hindrance from both the bulky cryptophane and folate group appended to the peptide. Removal of excess TCEP using a gel filtration column, prior to Cy3 addition, did not improve the yield.

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these cells exhibit relatively little folate uptake. After 4 h incubation with Cy3-labeled 25, fluorescence was seen evenly distributed in the perinuclear region of KB cells as expected for receptor-mediated endocytosis (Figure 1A). This was desirable as nuclear internalization of imaging agents can cause potential mutagenic effects on healthy cells. Uptake of Cy3-labeled 25 in HeLa cells was also confirmed by CLSM after 4 h incubation (Figure 1B). The fluorescence intensity was lower in HeLa cells than in KB cells, which was in agreement with previous studies. Uptake of 25 was negligible in HT-1080 (FR−) cells, thereby indicating that biosensor 25 was able to discriminate between FR+ and FR− cells (Figure 1C). To analyze whether the uptake of 25 was facilitated by folate receptor-mediated endocytosis, 25 was coincubated with folic acid rich medium for all three cell lines. Because folic acid is known to have a very high affinity for FRα, excess folic acid was expected to outcompete 25, thereby blocking uptake. The reduction in fluorescence in Figure 1D–F indicated that 25 was specifically recognized by the FR receptor. Indeed, the folate recognition moiety was critical for cellular uptake of this biosensor.

**Cytotoxicity Studies.** The cytotoxicity of folate–cryptophane conjugate 24 was evaluated by incubating KB (FR+) and HT-1080 (FR−) cells with increasing concentrations (0 to 100 μM) of 24 for 24 h, as shown in Figure 2. In KB cells, the viability (scaled to 100% at 0 μM) decreased from 80% at 10 μM to 50% at 38 μM. Maximum toxicity in KB cells (23% viability) was found when the cells were incubated with the highest concentration of 24 (100 μM). Cell viabilities determined when 0–10 μM of the biosensor was added to KB cells were comparable to those seen previously with fluorescent contrast agents such as folate-substituted poly(p-phenyleneethynylene). At concentrations ~2 μM, 25 exhibited sufficient fluorescence intensity to be detected intracellularly via both confocal microscopy and flow cytometry and was also minimally cytotoxic. The viability of HT-1080 cells with 24 ranged from 100% at 0 μM to 82% at 100 μM. The greater cytotoxicity observed for KB cells was likely due to the higher levels of FRα that are expressed on KB cells versus HT-1080 cells, which in turn caused increased intracellular accumulation of the folate–cryptophane conjugates. Similar trends were seen in a previous study where a cyclic RGD peptide-conjugated cryptophane was determined to be more toxic in cell lines overexpressing the targeted receptors (60% toxicity in ASPC-1 cells versus 30% toxicity in HFL-1 cells) after 24 h incubation at 100 μM concentration.

**Quantifying Cellular Internalization with Flow Cytometry.** In an effort to quantify the selective cellular internalization of 25 in KB and HT-1080 cells, flow cytometry was performed (Figure 3). After 4 h incubation in both KB and HT-1080 cells, there was a dramatic increase in cell-associated fluorescence. When biosensor 25 was coincubated with excess folic acid, the increase in median fluorescence intensity was much lower than when folic acid was absent. This was in agreement with the results from the CLSM studies, where uptake was significantly reduced when excess folic acid was present. In the absence of folic acid, the median cell-associated fluorescence intensity was approximately 45-fold higher in KB cells.
cells and 3-fold higher in HT-1080 cells. Based on flow cytometry data, it was determined that the median fluorescence intensity in KB cells was approximately 10-fold higher than in HT-1080 cells, consistent with the expected levels of FRα expression. These data confirmed that 25 selectively targeted cancer cells overexpressing the intended folate receptors.

**Hyperpolarized $^{129}$Xe NMR.** Hyperpolarized $^{129}$Xe NMR spectra of 24 were acquired at 60 $\mu$M in acetate buffer at pH 5.0 using a 10 mm NMR probe and BURP-shaped soft pulse. Sample temperature was controlled by a VT unit on the NMR spectrometer to 300 ± 1 K. Chemical shifts were referenced relative to $^{129}$Xe gas at 0 ppm when extrapolated to 0 atm.

![Hyperpolarized $^{129}$Xe NMR spectrum of 60 $\mu$M 24 in acetate buffer at pH 5.0.](image)

Figure 4. Hyperpolarized $^{129}$Xe NMR spectrum of 60 $\mu$M 24 in acetate buffer at pH 5.0 (40 scans; $S/N = 30:1$ with 50 Hz line broadening).

Figure 4 shows a HP $^{129}$Xe-aq NMR peak at 195.0 ppm and $^{129}$Xe NMR chemical shifts of 64.8 and 66.0 ppm corresponding to diastereomers of 24. This was due to the chirality of the three components—folate, peptide, and cryptophane (LRL and LRR). Cryptophane-A is a chiral molecule and the racemic mixture of two enantiomers encapsulating xenon is known to give rise to a single $^{129}$Xe NMR resonance in water. However, upon conjugation of chiral moieties to racemic cryptophane, diastereomers are formed. Previous examples of xenon biosensor diastereomers include the biotin-conjugated cryptophane developed by Spence et al. The biosensor consisted of four diastereomers due to the chiral cryptophane, L-amino acids, and maleimide center formed when the biotin was conjugated to the rest of the biosensor (RLR, RLL, LLR, LLL). This resulted in 4 distinct peaks in the $^{129}$Xe NMR spectrum. Similarly, the enzyme MMP-7 biosensor developed in our laboratory indicated the presence of two diastereomers that were separated by 0.6 ppm. This was due to the chirality of the two components, peptide and cryptophane-A (RL and LL).

Our HP $^{129}$Xe NMR studies with folate binding protein (FBP) and 24 resulted in no observable protein bound signal (Supporting Information, Figure S11). FBP is a membrane-bound protein and is known to aggregate at low micromolar concentrations. It was necessary, therefore, to investigate experimental conditions where the protein is maximally stable (30 $\mu$M FBP, 30 and 60 $\mu$M biosensor 24 in acetate buffer, pH 5.0 with and without 10% glycerol; vortex mixed and incubated 30 min). The $^{129}$Xe NMR peaks for 24 in the presence of FBP (at 66.7 and 68.0 ppm, Figure S11) were essentially identical to those shown for 24 in the absence of FBP (Figure 4). However, it is important to emphasize that the biosensor need not induce a chemical shift change to be useful in vivo. As we have demonstrated with the confocal microscopy and flow cytometry studies, the biosensor should preferentially localize in FR+ cells as the free biosensor is diluted in circulation. Thus, detection of HP $^{129}$Xe NMR signal corresponding to the cryptophane biosensor will indicate FR+ tissue. Recent improvements in $^{129}$Xe hyperpolarization methods and HP $^{129}$Xe cellular NMR techniques should make it possible using similar folate-cryptophane biosensors in the future to discriminate between FR+ and FR− cells by $^{129}$Xe NMR.

### CONCLUSIONS

In summary, a water-soluble, folate- and Cy3-conjugated biosensor was synthesized in 20 nonlinear steps and fully characterized. During conjugation, the folate moiety was selectively protected to ensure that only the α-carboxylate group was available to bind to FRα. Confocal imaging with FR+ and FR− cells confirmed the selective uptake of biosensor via folate receptor-mediated endocytosis by cells overexpressing FRα. Flow cytometry analysis quantified that uptake was 45-fold higher in KB cells and 3-fold higher in HT-1080 cells than when competing excess folate was in solution. Also, the median fluorescence intensity was approximately 10-fold higher in KB cells than HT-1080 cells, which motivates the use of folate-conjugated cryptophane for in vivo biosensing in cells overexpressing FRα. Cytotoxicity assays indicated that in the relevant concentration range required for confocal and flow cytometry analysis (1–10 $\mu$M), the viability was greater than 80% in both cell lines. Further advances in efficient cryptophane synthesis will make it more practical in the future to generate folate-cryptophane biosensors in larger quantities needed for cell or in vivo $^{129}$Xe NMR studies.

### EXPERIMENTAL PROCEDURES

**Reagents. Sigma-Aldrich.** Dimethyl sulfoxide (DMSO), dimethylformamide (DMF), folate binding protein (FBP), folic acid, methanol, triisopropylsilane (TIPS, 99%), 2,6-lutidine, piperidine, 3-(4,5- dimethyl-2-thiazolyl)-2,5-diphenyl-2H-tetrazolium bromide (MTT). Fisher. Sodium chloride, copper(II) sulfate, trifluoroacetic acid (TFA), diethyl ether (Et2O).

**Alfa Aesar.** Cesium carbonate, l-glutathione. Novabiochem. 2-(1H-benzotriazole-1-yl) 1,1,3,3-tetramethyldisilazane, (HBTU), N-hydroxybenzotriazole (HOBT), N-methylmorpholine (0.4 M), Fmoc-15-amino-4,7,10,13 tetraoxapentadecanoic acid ([PEG]15), rink amide resin, Fmoc-protected amino acids including Fmoc-l-Lys(vDde)-OH, Fmoc-l-Lys(Boc)-OH, Fmoc-l-Arg(Pbf)-OH, Fmoc-Cys(tButhio)-OH, N-methylmorpholine (0.4 M).

**GE Healthcare.** Cy3 monoreactive dye pack.

**Calbiochem.** Tris(2-carboxyethyl)phosphine hydrochloride (TCEP-HCl).

**Invitrogen.** RPMI-1640 medium, folate-depleted RPMI-1640 medium, Dulbecco’s phosphate buffered saline (DPBS). For biological assays, all solutions were prepared using deionized water purified by Mar Cor Premium grade Mixed Bed Service Deionization.
**Bioconjugate Chemistry**

### General Methods.

All organic reactions were carried out under nitrogen atmosphere. ¹H NMR (500.14 MHz) and ¹³C NMR (125.77 MHz) spectra were obtained on a Bruker AMX 500 spectrometer at the University of Pennsylvania Chemistry Department NMR facility. Electrospray ionization (ESI) mass spectrometry was performed in low-resolution mode on a Micromass LC Platform and in high-resolution mode on a Micromass Autospec. Matrix-assisted laser desorption/ionization mass spectrometry (MALDI-MS) was performed on a Bruker Daltonic Ultraflex III MALDI-TOF/TOF spectrometer at the Mass Spectrometry Center in the Chemistry Department at the University of Pennsylvania. Column chromatography was performed using 60 Å porosity, 40 μm silica gel plates with UV light at 254 nm from Sorbent Technologies. Thin layer chromatography (TLC) was performed using silica gel plates with UV light at 254 nm.

**Synthesis of 7.** α-[2-(Trimethylsilyl)ethoxy]-2-N-[2-(trimethylsilyl)-ethoxycarbonyl]folic acid (7) was prepared according to literature procedures and matched the reported physical constants and NMR spectra.

**Synthesis of 21.** Monopropargyl cryptophane was prepared according to literature procedures and matched the reported physical constants and NMR spectra.

**Synthesis of 22.** Peptide 22 (Scheme 2) was prepared by solid-phase synthesis using standard Fmoc amino acid protection chemistry on Rink Amide resin (0.1 mmol scale). Couplings of Fmoc-protected amino acids to the resin were carried out with HBTU and N-methylmorpholine, 1 equiv) was added. The suspension was degassed with N₂ and allowed to stir for 10 min. 2,6-Diiodo-6-bromo-p-phenylene (18.2 mg on solid support, maximum 0.01093 mmol azidepeptide, 1 equiv) and allowed to stir for 10 min. 2,6-Lutidine (0.0219 mmol, 1 equiv) was added and the reaction mixture was degassed. Sodium ascorbate (0.4372 mmol, 40 equiv) was added dropwise, the mixture was degassed, and finally an aqeous solution of copper(II) sulfate (0.0054 mmol, 0.5 equiv) was added. The suspension was degassed with N₂ and stirred at rt for 24 h. The resin was then carefully filtered using a peptide vessel, and water (90/5/S) at rt at 4 h. The reaction mixture was filtered using a peptide vessel, and the peptide was precipitated by the addition of ether. The cleavage cocktail removed side chain protecting groups from all amino acids except for the t-butylthiol-protected cysteine. Semipreparative HPLC purification of 22 was accomplished using the following gradient: time 0, A/B = 95/5; 0–45 min, linear increase to A/B = 50/50; 45–47 min, linear increase to A/B = 20/80; 47–56 min, linear change to A/B = 20/80; 56–57 min, linear increase to A/B = 95/5; 57–72 min, linear change to A/B = 95/5 (SI, Figure S3). MALDI-MS calculated for peptide 22, C₁₂H₁₄₁N₃₁O₁₆S₂ (M + H⁺) 1761.06; found 1760.91 (SI, Figure S4).

**Synthesis of 23.** Peptide 22 on the Rink Amide resin (30 mg, maximum, 0.0201 mmol azido peptide 22, 1 equiv) was allowed to swell in DMF (500 μL) in a 10 mL peptide vessel for 10 min. The solution was filtered and 1 mL of 4% hydrazine in DMF was added to deprotect the iVDe group on the orthogonally protected lysine. This was repeated 5 times and the absorption of the filtrate at 290 nm was measured by UV−vis spectroscopy to ensure that deprotection had taken place. The resin was dried under vacuum. 22 was then added to a mixture of 7 (0.0402 mmol, 2 equiv), HBTU (0.0603 mmol, 3 equiv), HOBT (0.0905 mmol, 4.5 equiv), and DIEA (0.1206 mmol, 6 equiv) in dry DMF. The reaction was stirred overnight at rt under nitrogen. Once the reaction was complete, the resin was carefully transferred to a fritted reaction vessel and washed sequentially with DMF, CH₂Cl₂, MeOH, 1:1 MeOH/CH₂Cl₂, and MeOH before drying under vacuum. The peptide coupled to folate 23 was cleaved from the resin using a mixture of TFA, TIPS, and water (90/5/S) at rt for 4 h. The reaction mixture was filtered using a peptide vessel, concentrated, and the peptide was precipitated by the addition of ether. The cleavage cocktail removed side chain protecting groups from all amino acids except for the t-butylthiol-protected cysteine. Semipreparative HPLC purification of 23 was accomplished using the following gradient: time 0, A/B = 95/5; 0–45 min, linear increase to A/B = 50/50; 45–47 min, linear increase to A/B = 20/80; 47–56 min, linear change to A/B = 20/80; 56–57 min, linear increase to A/B = 95/5; 57–72 min, linear decrease to A/B = 95/5 (SI, Figure S5). MALDI-MS calculated for peptide−folate conjugate 23, C₀₉H₁₅₅N₃₈O₂₁S₂ (M + H⁺) 2184.19; found 2184.05 (SI, Figure S6).

**Synthesis of 24.** Monopropargyl cryptophane 21 (20 mg, 0.02186 mmol, 2 equiv) in 900 μL dry DMSO was added to 23 (18.2 mg on solid support, maximum 0.01093 mmol azido peptide, 1 equiv) and allowed to stir for 10 min. 2,6-Lutidine (0.0219 mmol, 1 equiv) was added and the reaction mixture was degassed. Sodium ascorbate (0.4372 mmol, 40 equiv) was added dropwise, the mixture was degassed, and finally an aqueous solution of copper(II) sulfate (0.0054 mmol, 0.5 equiv) was added. The suspension was degassed with N₂ and stirred at rt for 24 h. The resin was then carefully filtered using a peptide vessel, and water (90/5/S) at rt at 4 h. The reaction mixture was filtered using a peptide vessel, concentrated, and the peptide was precipitated by the addition of ether. The cleavage cocktail removed side chain protecting groups from all amino acids except for the t-butylthiol-protected cysteine. Semipreparative HPLC purification of 24 was accomplished using the following gradient: time 0, A/B = 95/5; 0–65 min, linear increase to A/B = 30/70; 65–68 min, linear increase to A/B = 20/80; 68–70 min, linear increase to A/B = 5/95 (SI, Figure S7). MALDI-MS calculated for 24, C₁₁₂H₁₃₁N₅₈O₅₂S₂ (M + H⁺) 3102.61; found 3103.08 (SI, Figure S8).

**Synthesis of 25.** Cys-protected folate-peptide-cryptophane conjugate 24 was dissolved in PBS buffer (100 mM, pH 7.1) at a concentration of 60 μM. The GE protocol was followed to deprotect the t-butylthiol group and label the cysteine with the Cy3-maleimide construct. TCEP (0.0006 mmol, 10 equiv) was added to a 1 mL PBS solution containing 24 and degassed. The solution was stirred for 40 min to which was added Cy3 dye
dissolved in 50 μL dry DMSO. The reaction was degassed and stirred under nitrogen at rt for 16 h. The reaction mixture was purified by HPLC using the following gradient: time 0, A/B = 95/5; 0–65 min, linear increase to A/B = 30/70; 65–68 min, linear change to A/B = 20/80; 68–70 min, A/B = 5/95 (SI, Figure S9). MALDI-MS calculated for C_{180}H_{253}N_{42}O_{42}S_{3} (M+H+) 3771.81; found 3771.59 (SI, Figure S10). Extinction coefficients used to determine solution concentrations of Cy3-labeled 25 were ε_{380} = 38 000 M^{-1} cm^{-1} and ε_{552} = 150 000 M^{-1} cm^{-1} in water.

**Cell Culture.** KB, HeLa, and HT-1080 cells were obtained from Dr. Jerry Glickson (University of Pennsylvania, Perelman School of Medicine, Philadelphia, PA). All cells were grown in 25 cm² tissue culture flasks in RPMI-1640 with 25 mM HEPES supplemented with 2 mM L-glutamine, 15% fetal calf serum, 100 units penicillin, and 100 units streptomycin. Cells were subcultured on a weekly basis.

**Cell Viability (MTT) Assay.** In 96 well plates 25 000 KB or HT-1080 cells were plated per well and allowed to grow overnight. A stock solution of non- fluorescently labeled folate-peptide-cryptophane conjugate 24 was added to wells in triplicate at final concentrations of 0, 2, 10, 25, 50, 75, and 100 μM and incubated for 24 h in the dark. The medium was aspirated and the cells were washed thrice with DPBS before being treated with 20 μL of MTT (5 mg/mL) for 3 h. The medium was removed and DMSO was added to solubilize the resulting crystals. A Labsystems Fluoroskan II microplate reader was used to record the absorbance at 540 nm. Absorbance readings were subtracted from the value of wells containing untreated cells, and the reduction in cell growth was calculated as a percentage of control absorbance in the absence of any treatment. Data show the mean of at least three independent experiments ± SD.

**Cell Uptake Studies.** KB, HeLa, and HT-1080 cells were grown to confluence on LabTek 8-well microscope slides with glass coverslip bottoms at a density of 50 000 cells per plate. The cells were grown in folate-depleted media for 24 h prior to incubation with 4 μM solution of Cy3-labeled 25 for 4 h at 37 °C. For blocking studies, cells were grown in media containing folic acid for 24 h prior to incubation with 25 under the same conditions mentioned above. The medium was removed and the cells were washed three times with DPBS. Cells were visualized using an Olympus FV1000 confocal laser scanning microscope with 543 nm (HeNe) laser excitation and Cy3 emission filter under 40X magnification (Olympus UApO/340, 1.15 NA water objective).

**Flow Cytometry Experiments.** KB and HT-1080 cells were seeded in T25 flasks each containing 10⁵ cells and grown for 1 day in folate-depleted RPMI-1640 medium. The cells were incubated for 4 h with 4 μM 25 (1.3 mL/flask). For blocking studies, 4 μM 25 was added in the presence of medium containing folic acid. The medium was aspirated and cells washed 3 times with 2 mL PBS. The cells were detached using trypsin-EDTA and centrifuged. The supernatant was aspirated and resuspended in 650 μL 10% FBS in Dulbecco’s PBS and immediately analyzed on a BD LSRII machine at the Flow Cytometry Laboratory, Abramson Cancer Center, at the University of Pennsylvania.

**129Xe NMR.** Hyperpolarized 129Xe was generated using a home-built 129Xe hyperpolarizer, which is based on the formerly commercially available Nycomed-Amersham (now GE) IGLXe.2000 system. A gas mixture of 10% N2, 89% He, and 1% natural abundance Xe (Spectra Gases) was flowed through the hyperpolarizer. 129Xe was hyperpolarized to 10–15% after having been cryogenically separated, accumulated, thawed, and collected in CAV NMR tubes (New Era). After Xe collection, NMR tubes were shaken vigorously to mix cryptophane solutions with Xe. All 129Xe NMR measurements were carried out on a 500 MHz Bruker BioDRX NMR spectrometer. RF pulse frequency for 129Xe was 138.12 MHz. Samples were observed using a 10 mm PABBO NMR probe. 129Xe NMR spectra were acquired using the exchange signal averaging (ESA) method. 54 Selective pulses (90 degree flip angle, EBURP-1 shaped) were generated at the Xe@cryptophane resonance frequencies. Each pulse lasted 5 ms, which gave a designated excitation region 1 kHz (7.2 ppm). All spectra were signal averaged by 40 scans. A delay of 0.15 s was given between scans to allow polarized Xe to exchange in and depolarized Xe to exchange out of the cryptophane cavity. The natural line widths of Xe@cryptophane peaks are around 80 Hz (fwhm, Lorentzian fitted). The spectra shown above are exponentially broadened by 100 Hz, to give a larger signal/noise ratio. Sample temperature was controlled by a VT unit on the NMR spectrometer to 27 ± 1 °C.

**ASSOCIATED CONTENT**

**Supporting Information**

HPLC, MALDI-MS, and NMR characterization. This material is available free of charge via the Internet at http://pubs.acs.org.

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**Notes**

The authors declare no competing financial interest.

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