MRI measurements of reporter-mediated increases in transmembrane water exchange enable detection of a gene reporter

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Non-invasive imaging of gene expression can be used to track implanted cells in vivo but often requires the addition of an exogenous contrast agent that may have limited tissue access1. We show that the urea transporter (UT-B) can be used as a gene reporter, where reporter expression is detected using 1H MRI measurements of UT-B-mediated increases in plasma membrane water exchange. HEK cells transfected with the reporter showed an increased apparent water exchange rate (AXR), which increased in line with UT-B expression. AXR values measured in vivo, in UT-B-expressing HEK cell xenografts, were significantly higher (about twofold, \( P < 0.0001 \)), compared with non-expressing controls. Fluorescence imaging of a red fluorescent protein (mStrawberry), co-expressed with UT-B showed that UT-B expression correlated in a linear fashion with AXR. Transduction of rat brain cells in situ with a lentiviral vector expressing UT-B resulted in about a twofold increase in AXR at the site of virus injection.

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Most imaging gene reporters are receptors, enzymes, or membrane transporters that generate image contrast by interaction with an exogenous imaging agent1. Imaging reporter expression in vivo could be used in the clinic to monitor delivery of gene therapy vectors or for cell tracking in regenerative medicine and in immunotherapy2,3. Compared with direct labeling approaches that preload cells with contrast agents, gene reporters have the advantage that contrast arises from protein expression, which reports indirectly on cell viability, and that the signal is not diluted after cell division. Moreover, if the reporter is expressed from a tissue-specific promoter the location of the cell and its differentiation state can be detected.

Various gene reporters have been described for use with MRI, where these rely on different underlying contrast mechanisms4 with most using exogenous contrast agents that alter longitudinal (\( T_1 \)) or transverse relaxation times (\( T_2, T_2^* \))5. Reporters that produce endogenous contrast are potentially more useful, because they do not require contrast agent delivery. Endogenous reporters include those that accumulate iron, such as tyrosinase, transferrin, MagA and ferritin, although they may need to be supplemented with exogenous iron6,7. Another endogenous reporter is the lysine-rich protein (LRP), which contains multiple exchangeable amide protons that can be detected using chemical exchange saturation transfer (CEST)8,9. We recently identified a gene reporter based on the urea transporter (UT-B), whose expression was detected in vivo using 13C magnetic resonance spectroscopy measurements of the apparent diffusion coefficient (ADC) of injected hyperpolarized 13C urea10. UT-Bs also function as aqueous channels, transporting water at rates similar to aquaporins11. Therefore, we hypothesized that UT-B expression might also be detectable by 1H MRI measurements of water exchange across the plasma membrane, thus allowing imaging of gene expression.

Intracellular water diffusion is restricted by the plasma membrane and hindered by intracellular macromolecules, resulting in a lower apparent diffusion coefficient for intracellular as compared to extracellular water12. Filter exchange spectroscopy (FEXSY) uses a “diffusion filter” to remove magnetization from “fast-diffusing” extracellular water and then measures the return of the magnetization to equilibrium following water exchange between the extra- and intracellular compartments (Fig. 1a,b). An imaging version of FEXSY (filter-exchange imaging (FEXI)) can also be used to measure the apparent exchange rate (AXR) between these compartments13.

We used FEXI to detect UT-B transgene expression in vivo (see Supplementary Note 1 and Supplementary Figs. 1 and 2 for validation of this imaging methodology), and introduce this as a new endogenous MRI gene reporter that produces higher levels of contrast than endogenous reporters described previously.

HEK 293T cells were transduced with a vector co-expressing, via an E2A sequence, luciferase and the red fluorescent protein, mStrawberry, or a vector co-expressing mStrawberry and UT-B (Fig. 1c). The levels of mStrawberry fluorescence provided a surrogate measure of luciferase and UT-B protein expression. We used these cells to derive six different cell lines, five of which expressed UT-B. Lines included a monoclonal control cell line expressing luciferase and mStrawberry (EF1-I-S), a polyclonal line expressing mStrawberry and UT-B (polyclonal EF1-S-UTB), and monoclonal populations isolated using single-cell-sorting for low and high mStrawberry expression, co-expressing low and high levels of UT-B (EF1-S-UTB low, and
EF1-S-UTB high), respectively (Supplementary Fig. 3). We also used the PGK-S-UTB cell line, which we used previously in urea transport studies10. Very high levels of UT-B expression were measured in EF1-S-UTB high cells (Fig. 1j and Supplementary Fig. 3), which inhibited their growth (Fig. 1d). Water transport by UT-B was assessed by measuring decreased cell viability after incubation in hypotonic salt solutions for 5 min. In a hypotonic 0.225% salt solution expression of UT-B resulted in up to 47% and 24% decreases in viability of EF1-S-UTB high cells and EF1-S-UTB low cells, respectively, when compared to control cells.

This effect was partially reversed by addition of the UT-B inhibitor N,N′-dimethylthiourea, showing that at these expression levels UT-B mediates relatively rapid water transport across the plasma membrane (Fig. 1e).

FEXI images of pellets of HEK 293T, EF1-L-S, polyclonal, EF1-S-UTB, EF1-S-UTB low, and EF1-S-UTB high cell lines, revealed an increase in AXR in parallel with increases in UT-B expression (Fig. 1f–i). When corrected for background levels of water transport (in HEK 293T and EF1-L-S cells) the increase in AXR correlated with the increase in UT-B expression, as determined from measurements of UT-B mRNA levels using real-time PCR (Fig. 1j, Supplementary Fig. 4, Spearman \( r = 1, P = 0.0083 \); linear regression with \( R^2 = 0.88 \) and slope significantly different from zero, \( P = 0.018 \)). Cell viability was >95% before and after imaging. Inhibition of UT-B transporter activity in the EF1-S-UTB high cell line, with 170 mM N,N′-dimethylthiourea, decreased AXR (\( P < 0.001, \) Mann-Whitney-Wilcoxon test) to a value similar to that observed in control cells (Fig. 1h,i).

To assess whether exchangeable protons on intracellular proteins might contribute to the measured AXR, we performed measurements on solutions of 35% w/w and 4% w/w bovine serum albumin (BSA). At both high and low BSA concentrations, there was no measurable AXR (Supplementary Fig. 5).
with a mean AXR of 3.45 ± 0.52 s⁻¹ for EF1-S-UTB low (n = 8), 3.25 ± 0.58 s⁻¹ for EF1-S-UTB high (n = 4), 3.30 ± 1.18 s⁻¹ for PGK-S-UTB (n = 8), 1.48 ± 0.64 s⁻¹ for HEK 293T (n = 8), and 2.05 ± 0.39 s⁻¹ for the EF1-L-S (n = 10) xenografts (representative fits from each group are shown in Fig. 2c). Individual AXR and mean values are shown in Figure 3c. Filter efficiency maps (Fig. 2d) showed reduced filter efficiency in all xenografts, when compared to surrounding tissue. AXR maps (Fig. 2e) identified UT-B expressing cells as areas with high transmembrane water exchange, which allowed non-invasive imaging of reporter gene expression with a spatial resolution of 0.93 mm × 0.93 mm × 3 mm. Fluorescence imaging confirmed expression of the UT-B transgene, which was co-expressed with the mStrawberry transgene. Xenograft/flank mean fluorescence intensity ratios were highest in the xenografts grown from cells that had been sorted for the highest levels of red fluorescence; EF1-L-S (2.88 ± 0.46) and EF1-S-UTB high (3.22 ± 0.07), whereas lower fluorescence intensity ratios were observed for PGK-S-UTB (1.31 ± 0.14) and EF1-S-UTB low xenografts (1.23 ± 0.08), as compared to the background from HEK 293T cells (0.95 ± 0.08, Fig. 2f). The similar fluorescence intensity ratios for PGK-S-UTB and EF1-S-UTB low xenografts were consistent with their similar AXR values. T1 and ADC values did not show significant differences between UT-B-expressing and control xenografts (Fig. 3a,b), whereas AXR and fluorescence measurements consistently detected transgene expression (Fig. 3c,d). Remarkably, MRI measurements of AXR had a similar sensitivity to the fluorescence measurements for detecting transgene expression (Fig. 3c,d), with the caveat that red fluorescence is typically detected from penetration depths up to a few millimeters, whereas the MRI measurements were collected from a 3 mm thick slice. Moreover, the contrast was higher for the MRI measurements (AXR was 2.33× higher in EF1-S-UTB low as compared to HEK 293T xenografts, whereas the ratio of the xenograft/flank mean fluorescence intensity ratios was only 1.30).

The xenograft/flank mean fluorescence intensity ratio correlated with the AXR values (Spearman r = 0.64, P = 0.0008; linear regression with R² = 0.42 and slope significantly different from zero, P = 0.0006, Fig. 3f), demonstrating that AXR can be used as a quantitative readout of UT-B gene expression. However, the negative selection pressure imparted by the lower growth rate of the EF1-S-UTB high cells (Fig. 1d) was manifest in the EF1-S-UTB high xenografts as a loss of UT-B mRNA expression (Fig. 3e) and an AXR value that was lower than in the EF1-S-UTB low xenografts (Fig. 3c). Immunostaining confirmed that mStrawberry expression was higher in the EF1-L-S and EF1-S-UTB high xenografts than in the EF1-S-UTB low xenografts and HE&E staining showed that this had no discernible effect on cell viability in the xenografts (Supplementary Fig. 6).

Rat brain cells were transduced in vivo by direct intracranial injection of lentiviruses encoding either mStrawberry and UT-B (S-UTB), luciferase and mStrawberry (L-S) or a 50:50 mixture of the two lentiviruses. There was about a twofold increase in AXR at the site of injection of lentivirus encoding S-UTB when compared with controls that received only the L-S virus (n = 6 animals, n = 2 per injection; Fig. 4a,b and Supplementary Video 1). Viral transduction was confirmed in the animals that received the L-S virus by bioluminescence imaging of luciferase and mStrawberry (L-S) or a 50:50 mixture of the two lentiviruses. There was about a twofold increase in AXR at the site of injection of lentivirus encoding S-UTB when compared with controls that received only the L-S virus (n = 6 animals, n = 2 per injection; Fig. 4a,b and Supplementary Video 1). Viral transduction was confirmed in the animals that received the L-S virus by bioluminescence imaging of luciferase expression (Fig. 4c) and by histological staining for mStrawberry in all rats (Fig. 4d and Supplementary Fig. 7). ROIs analysis of the needles track, observed in the T2-weighted images (Fig. 4a), and an ROI on the contralateral side of the brain confirmed an increase in AXR in brain regions injected with virus encoding for UT-B (Fig. 4e).
The AXR was 2.95 ± 0.79 s⁻¹ (n = 8) from all non UT-B expressing regions (L-S and control) and 6.54 ± 2.66 s⁻¹ (n = 4) from UT-B expressing regions (mean ± s.d.; P ≤ 0.05, Mann-Whitney-Wilcoxon test). The mStrawberry-positive cells in the ROIs highlighted in (Fig. 4d) constituted 22.4 ± 12.3% of all cells.

The 200% higher AXR values in both UT-B-expressing xenografts (Fig. 3c) and in transduced brain cells in vivo (Fig. 4e) mean that UT-B is the most sensitive endogenous contrast mechanism MRI gene reporter to date, to our knowledge. For example, lysine-rich protein gave only a 4.7% enhancement, tyrosinase, a 35% increase in R₂ (Supplementary Table 1). Detection of UT-B expression using AXR measurements is similar conceptually to CEST measurements of lysine-rich protein expression. However, in contrast to these measurements, in which rapid exchange of protons between micro- to millimolar concentrations of lysine-rich protein (Supplementary Note 2) and intracellular bulk water is measured (the proton exchange rate for poly-L-lysine is 403 s⁻¹; ref. 18), FEXI measures exchange between a much larger pool of protons in intracellular water (>40 M) and the extracellular water pool, albeit at a much slower exchange rate (~4–6 s⁻¹AXR). The much larger pool size of intracellular water, when compared to the water-exchangeable protons bound to lysine-rich protein, compensates for the slower transmembrane exchange measured by FEXI. CEST detection of LRP might be improved by using more sophisticated methods for measuring CEST contrast. Nevertheless, comparison of the contrast-to-noise ratio (CNR) and CNR efficiency of the in vivo FEXI data presented here with CEST data from a recent study shows that FEXI detection of UT-B is more sensitive (CNR of 4.3 versus 1.6 and CNR efficiency of 1.1 versus 0.5; Supplementary Table 2). FEXI has a second advantage compared with CEST in that contrast can only arise from intact cells.

Cell dilution experiments in vitro (Supplementary Fig. 8) and our lentivirus experiments in vivo (Fig. 4) indicate a UT-B detection sensitivity of 10⁴–10⁵ cells/voxel (Supplementary Note 3), which is similar to the limit for 19F NMR detection of cells labeled with fluorinated tracers. Modeling experiments presented in Supplementary Figure 9 predict that detection of UT-B at lower cell densities might be possible.

The sensitivity of AXR measurements depends on the extent to which the diffusion filter suppresses extracellular signal, and on the background water exchange rate. Background AXR might change owing to other factors, such as inflammation, which has the potential to confound measurements of UT-B expression. One drawback of FEXI is the limited spatial resolution (~0.94 × 0.94 × 3 mm³ in the current study) because of the loss of signal resulting from the use of two diffusion modules. 3D-FEXI implementations using retrospective gating and slab-selective diffusion filtering could be used to improve both signal-to-noise ratio and spatial resolution, especially if combined with parallel imaging. Sensitivity might also be improved by increasing UT-B expression, although when highly expressed (>700 µM, see Supplementary Note 2), it can inhibit cell growth in vitro (Fig. 1d) and result in loss of expression in proliferating cells in vivo (Fig. 3e). An inducible system for UT-B gene expression might be helpful, or other water channels, such as the aquaporins, could be adopted because they transport water at similar rates to UT-B but have a different mechanism and therefore might not inhibit cell growth upon overexpression. Even though low levels of UT-B expression did not affect cell growth in vitro, the long-term effects of UT-B expression on cell function will need to be examined.
The FEXI experiment described here could be used in the clinic. Although sensitivity would decrease at the lower magnetic field strengths used in the clinic (about threefold at 3 T) magnetic field homogeneity would be improved, making the echo-planar imaging (EPI) readout used in the FEXI experiment less prone to artifacts.

In summary, we report that UT-B can be used as a gene reporter for MRI, free of contrast agent, that relies on endogenously generated contrast, and whose expression is detected by increases in transmembrane water exchange. The UT-B reporter could be applied to track cells non-invasively, to analyze cellular differentiation states in vivo or to monitor the delivery and expression of gene therapy vectors.

METHODS

Methods, including statements of data availability and any associated accession codes and references, are available in the online version of the paper.

Note: Any Supplementary Information and Source Data files are available in the online version of the paper.

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AUTHOR CONTRIBUTIONS

F.S., S.R., and K.M.B designed the research; F.S., S.R., D.-E.H., P.D., S.M., R.M., A.J.W., E.M., and A.A.N performed the research; F.S., S.R., and A.A.N. analyzed the data; S.R. generated the virally transduced cell lines and lentiviral particles, R.J.M.F contributed the brain model; and F.S. and K.M.B wrote the paper.

COMPETING FINANCIAL INTERESTS

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Sucrose phantom. For diffusion measurements and gradient calibrations, a phantom containing different sucrose concentrations was prepared\(^2\). Five microtainer tubes (Beckton, Dickinson and Company, Franklin Lakes, USA) containing 10–50% w/v sucrose (in 10% increments) were placed in a 50-mL cylindrical tube filled with water (Corning Incorporated, Corning, USA), giving final sucrose concentrations of 0.3–1.5 M.

Cell culture. Human embryonic kidney cells (HEK 293T) were obtained from the Cancer Research UK Cambridge Institute Biorepository. The cells were authenticated using short-tandem repeat genetic profiling (STR) yielding a 100% match to the HEK 293T cell line published on ATCC database. Mycoplasma tests were negative. Cells were grown in Dulbecco’s modified Eagle’s medium, with 10% FBS, and 5% l-glutamine, in 5% CO\(_2\) at 37°C. Cells were passaged when in exponential growth phase at 80% confluency. Cell viability and total cell count were assessed using an automated Trypan blue dye exclusion assay (ViCell, Beckman Coulter, High Wycombe, UK).

MRI experiments in vitro used –1.6 × 10\(^5\) cells, which were washed with phosphate-buffered saline (PBS), concentrated to give a dense cell suspension (800 g, 5 min, 4°C), transferred with a 1 ml pipette into 0.6 ml Eppendorf tubes and then centrifuged again at moderate speed to remove air bubbles (20g, 5 min, 4°C). UT-B activity was inhibited by incubating the cells with 170 mM N-N’-dimethylthiourea (10 min, 37°C) before they were pelleted, as above, and imaged.

DNA extraction, reverse transcription and qPCR. Total RNA was isolated from cells using an RNaseasy kit (Qiagen). Xenograft material, RNA was extracted using RLT Reagent (Qiagen, Venlo, the Netherlands) using the manufacturer’s protocol. Total RNA (1 µg) was used for first strand cDNA synthesis with SuperScript II Reverse Transcriptase and oligo dT primers (Invitrogen, Carlsbad, USA). Real-time PCR was performed with SYBR Green PCR Master Mix (Applied Biosystems, Waltham, USA) using Quantitect primers (Qiagen: Mm_SLC14a1 QT00117502; Hs_ACTB QT00095431; Hs_B2M QT00088935) in a QuantStudio 6 Flex Real-Time PCR System (Applied Biosystems, Waltham, USA). All reactions were performed in triplicate. The relative amount of all mRNAs was calculated using the comparative CT method after normalization to the Geomean of β-actin and β2-microglobulin (B2M).

Functional assay for UT-B expression. UT-B activity was assessed by placing cells in a hypoosmotic solution (0.225% NaCl) and assessing their viability. In this hypoosmotic medium UT-B-expressing cells, with faster transmembrane water transport, were expected to increase in volume at a greater rate than non-expressing cells and therefore show lower viability. Cells were grown to 60% confluence and then resuspended in 0.9% and 0.225% NaCl solutions, incubated on ice for 5 min, and then their viability and total cell count assessed using ViCell. For each experiment 50 images were analyzed and each experiment was repeated four times. Cell viability was defined as the percentage of unstained viable cells at 0.225% NaCl compared to the number at physiological salt concentration (0.9% NaCl). The quoted error is the s.d. of the mean value of the percentage of unstained viable cells in four independent experiments.

Cell implantation. Severe combined immune-deficient (SCID) mice, 6–8 weeks old, (Charles River Ltd, Margate, UK) were implanted subcutaneously with either 1 × 10\(^6\) control HEK 293T cells, or HEK 293T cells transfected with PGK-S-UTB, or EF1-S-UTB or EF1-S lentiviral vectors. The cells were suspended in PBS before injection. UT-B expressing cells were injected on the left dorsolateral flank and control cells on the contralateral flank. Prior to implantation, cells were counted and their viability assessed (ViCell). Imaging was performed using mice with similar xenograft burden. Xenograft volume was determined using the ellipsoidal volume formula: 1/2 × length × width\(^2\). Experiments were conducted in compliance with project and personal licenses issued under the Animals (Scientific Procedures) Act of 1986 and were designed according to the UK Co-ordinating Committee on Cancer Research guidelines for the welfare of animals in experimental neoplasia. The Cancer Research UK Cambridge Institute Animal Welfare and Ethical Review Body approved the work.

Viral transfection in vivo. Lentiviral particles were produced as described previously\(^2\) and titred using a MACSQuantVYB benchtop flow cytometer. Six-week-old (150–190 g) female CD IGS rats (Charles River UK Limited, Kent) were anaesthetized by inhalation of 1–2% isoflurane (Isoflo, Abbotts Laboratories Ltd., UK) in air/O\(_2\) (flow rate 2 L min\(^{-1}\)). Analgesia was administered subcutaneously (Vetregesic, Alstoe, York, UK) containing 0.3 mg/ml buprenorphine hydrochloride and 0.135% w/v chloroform diluted 1:10 in 0.9% sodium chloride, and 1 ml/kg of subcutaneous Rimadyl LA ( Pfizer, New York, USA) containing caropen 5 mg/kg diluted 1:10 in 0.9% sodium chloride). Respiratory rate was monitored at maintained at ~60 breaths min\(^{-1}\) with core body temperature maintained via a heat pad. Animals were transferred to a stereotactic surgical frame (Kopf, Tujunga, USA) and the head underwent three-point fixation using ear bars and a metal bit. The scalp was shaved and washed with aqueous Viden (Ecolab, USA). A midline incision was performed and pericranium stripped. A 1 mm Burr hole was drilled freehand at 2 mm anterior and 3 mm lateral to the bregma (right-side). A 23-gauge full displacement syringe (SGE Analytical Science, Melbourne, Australia) was filled with 5 µl of virus mixture at 1.7 × 10\(^{10}\) viral particles µl\(^{-1}\) before being inserted 6 mm intracranially. Upon withdrawal by 1 mm, the contents of the syringe were injected into the right caudate nucleus at 2 µl min\(^{-1}\). The syringe was removed over 30 s and the burr hole filled with bone wax (Ethicon, Norderstedt, Germany). Interrupted 6/0 undyed absorbable vicryl rapid sutures (Ethicon, Norderstedt, Germany) were used to close the wound, which was then covered using tissue glue (Glutuare, US) after which the animal was recovered in a hot box. Rimadyl LA (1:10 0.9% saline) was given for 48 h post-operatively as analgesia.

MRI. Magnetic resonance imaging was done using a 9.4 T horizontal bore small animal MRI scanner (Agilent, Palo Alto, USA) using a transmit-receive 4 cm inner diameter Millipede coil (Agilent, Palo Alto, CA). After placement of the animal in the scanner, scout images were acquired using 3D gradient echo and coronal fast spin echo sequences for animal positioning. First-order shimming was done using an automated non-selective FID-based procedure and was then further optimized using slice-selective manual shimming using a PRESS sequence. Line widths for 3 mm axial slices were ~90 Hz in vivo and 30 Hz in vitro. Mice were anesthetized by inhalation of 1.5 – 2.5% isoflurane (Isoflo, Abbotts Laboratories, Maidenhead, UK) in 75 air/25% O\(_2\) (2 l min\(^{-1}\)) delivered via a facemask. Body temperature was maintained by blowing warm air through the magnet bore. Breathing rate (30–40 b.p.m.) and body temperature (37°C) were monitored during experiments (Biotig, Small Animal Instruments, Stony Brook, USA). Respiratory triggering was used for all measurements such that images were acquired during the expiration phase. An axial slice of 3 mm thickness was positioned in the center of the two xenografts and a reference image was acquired using a fast spin echo sequence (repetition time ≥ 2 s, matrix size: 256 × 256, field of view (FOV): 3 cm × 3 cm, TE = 20 ms, turbo factor = 8). RF pulse power calibration was performed using a slice at the same spatial position but 5 mm thick. MRI of rat brains was performed
with the same protocol as described above but on a 7 T horizontal bore scanner (Agilent, Palo Alto, USA) using a 72-mm transmit coil with a rat head quadrature receive coil (Rapid Biomedical, Rimpar, Germany) using a FOV of 4 cm × 4 cm.

Filter-exchange imaging and data analysis. A filter-exchange imaging (FEXI) sequence was optimized using a phantom containing different compartments with sucrose concentrations in the range of 0.3 to 1.5 M. Sucrose-water solutions serve as a simple two-compartment model system, consisting of a fast-diffusing free water and slow diffusing bound water. The principles of the FEXI sequence are illustrated in Figure 1a in the main text. Application of the diffusion filter suppresses signal from the apparently fast diffusing water (in this case in the extracellular space) leading to a reduction in the measured ADC, denoted $ADC'_{\text{syn}}$, compared to the ADC at equilibrium $ADC_{\text{ref}}$. The reduction in $ADC'$ compared to $ADC_{\text{ref}}$ directly after application of the diffusion filter is quantified by the filter efficiency $\sigma$, where $\sigma = 1 - ADC'_{\text{syn}}/ADC_{\text{ref}}$. With increasing mixing time, $tm$, between the filter and detection modules, exchange of water between the intra- and extracellular compartments leads to relaxation of $ADC'$ back to its equilibrium value, which is determined by the apparent exchange rate, $AXR$ (Fig. 1b). Assuming negligible effects from longitudinal and transverse relaxation and an exchange that is slow when compared to the timescale of the pulsed-field gradient spin echo blocks, this equilibration process can be described by the equation:

$$ADC' = ADC(1 - e^{-tm/AXR})$$  \(1\)

$T_1$-mapping and DWI. For $T_1$-mapping, an inversion recovery Turbo-FLASH sequence was used, which employed a non-slice-selective adiabatic inversion pulse with 15 inversion times (TI), which were acquired interleaved, between 0.1 s and 10 s (TI = 0.1; 0.4; 0.9; 1.8; 4; 0.2; 0.5; 1.2; 2.3; 6; 0.3; 0.7; 1.5; 2.8; 10 s). Images were acquired with an encoding matrix of 128 × 64; slice thickness, 3 mm; FOV, 3 cm × 3 cm; time between inversion pulses = 12 s. Total acquisition time was 3 min. Diffusion-weighted spin echo EPI was used for ADC measurements, with six $b$-values (1,228; 984; 740; 496; 250; 1 s/mm$^2$). Images were acquired with an encoding matrix size of 64 × 64; slice thickness, 3 mm; FOV, 3 cm × 3 cm; $\Delta = 0.012$ ms; diffusion gradient duration $\delta = 0.08$ ms. The sequence was triggered with a respiration sensor leading to a TR ≥ 3 s. Four averages were acquired in a segmented EPI readout ($n = 2$). Total acquisition time was ~4 min.

Fluorescence and bioluminescence imaging. At 2–3 weeks after cell implantation and immediately before the MRI measurements, mice were shaved at the site of implantation and the planar red fluorescence emission from transgenic cells imaged using an IVIS-200 camera (PerkinElmer, Waltham, MA). The animals were anesthetized using 2% isoflurane and 75% air/25% O$_2$ (flow rate 2 l min$^{-1}$), and the images analyzed using Living Image software version 4.4 (PerkinElmer). Images were acquired with epi-illumination, small binning, aperture range F2–F8, exposure 1–3 s, and the field of view was varied between 13 and 19.4 cm. The excitation and emission pass band ranges were 500–550 nm and 575–650 nm, respectively. A red background pass band correction filter (460–490 nm) was used to suppress autofluorescence. Rats were anesthetized and bioluminescence imaged using the IVIS-200 camera at ~5 min after luciferin injection (1 ml of 15 mg/ml solution i.p.).

Histology and immunohistochemistry. Sections of formalin-fixed, paraffin-embedded tissue (10 µm for xenografts and 5 µm for brain tissue) were stained with H&E or with an anti-RFP rabbit polyclonal antibody that crossreacts with mStrawberry (1:100 dilution) (Abcam ab34771) and detected using Leica’s Polymer Refine Kit in combination with the Bond automated system (Leica Biosystems DS9800). Slides were scanned at ×20 magnification with a resolution of 0.5 µm per pixel on an Aperio AT2 (Leica Biosystems). Images were analyzed using the Aperio Imagescope Nuclear version 9 algorithm to quantify the proportion of cells with positive nuclear staining.

Statistical analyses. All results are expressed as mean ± s.d. Statistical significance was tested using a Mann–Whitney–Wilcoxon test. Sample size estimates were not performed since both mean and s.d. had to be determined in the experiment for each group. Animal MRI experiments were not randomized and not blinded. Real-time PCR analysis of the xenografts was performed double-blinded, both during the experiment and during analysis.

Data availability. Image data and associated metadata can be accessed at: http://dx.doi.org/10.17863/CAM.4374

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