RESEARCH ARTICLE

Engineering tumor-specific catalytic nanosystem for NIR-II photothermal-augmented and synergistic starvation/chemodynamic nanotherapy

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Abstract

Background: As an emerging therapeutic modality, chemodynamic therapy (CDT), converting hydrogen peroxide (H2O2) into highly toxic reactive oxygen species (ROS), has been developed for tumor-specific therapy. However, the deficiency of endogenous H2O2 and high concentration of glutathione (GSH) in the tumor microenvironment (TME) weaken the CDT-based tumor-therapeutic efficacy. Herein, a photothermal-enhanced tumor-specific cascade catalytic nanosystem has been constructed on the basis of glucose oxidase (GOD)-functionalized molybdenum (Mo)-based polyoxometalate (POM) nanoclusters, termed as GOD@POMs.

Methods: GOD@POMs were synthesized by a facile one-pot procedure and covalently conjugation. Then, its structure was characterized by scanning electron microscope (SEM), transmission electron microscope (TEM), Fourier transform infrared (FTIR) spectroscopy and X-ray photoelectron spectroscopy (XPS). In addition, ultraviolet-visible-near-infrared (UV-vis-NIR) absorption spectrum and infrared thermal camera were applied to evaluate the catalytic and photothermal performance, respectively. Moreover, to confirm the therapeutic effects in vitro, cell counting kit-8 (CCK-8) assay, live/dead staining and ROS staining were performed. Furthermore, the biosafety of GOD@POMs was investigated via blood routine, biochemistry and hematoxylin and eosin (H&E) staining in Kunming mice. Besides, the C6 glioma tumor-bearing mice were constructed to evaluate its anti-tumor effects in vivo and its photoacoustic (PA) imaging capability. Notably, RNA sequencing, H&E, TdT-mediated dUTP nick end labeling (TUNEL) and Ki-67 staining were also conducted to disclose its underlying anti-tumor mechanism.

Results: In this multifunctional nanosystem, GOD can effectively catalyze the oxidation of intratumoral glucose into gluconic acid and H2O2, achieving the cancer starvation therapy. Meanwhile, the generated gluconic acid decreases the pH in TME resulting in POM aggregation, which enables PA imaging-guided tumor-specific photothermal therapy (PTT), especially in the second near-infrared (NIR-II) biological window. Importantly, the Mo (VI) sites on POM can be reduced to Mo (V) active sites in accompany with GSH depletion, and then the post-produced Mo (V) transforms...
Introduction
Currently, cancer is a kind of serious disease threatening public health. According to statistics, estimated 608,570 Americans died from cancer in 2021, corresponding to more than 1600 deaths per day [1]. The unmet clinical challenges encountered in cancer therapeutics, including drug resistance, high grade normal tissue toxicity and difficulty in deep tumor treatment, have led to the alternative approaches for development. Chemodynamic therapy (CDT), based on Fenton/Fenton-like reactions, introducing specific valence ions including iron (Fe), manganese (Mn), cobalt (Co), titanium (Ti), cerium (Ce) and copper (Cu) to react with endogenous hydrogen peroxide (H$_2$O$_2$) for generating more highly toxic and active reactive oxygen species (ROS) such as hydroxyl radicals (•OH) to kill tumor cells, is regarded as a promising tumor-therapeutic modality with high potential in clinical transformation [2–11]. However, a large amount of antioxidants mainly involving glutathione (GSH, up to 10 mM) exist in tumor microenvironment (TME), which plays a vital role in counteracting ROS-mediated oxidative damage during the treatment, thus the therapeutic effect of CDT is substantially neutralized [12, 13]. Furthermore, although tumor cells are gifted with relatively high H$_2$O$_2$ level (100 × 10$^{-6}$ to 1 × 10$^{-3}$ M) compared with normal cells, the endogenous H$_2$O$_2$ in the tumor region is generally insufficient to generate abundant •OH. Additionally, the occurrence and progress of Fenton/Fenton-like reaction demands rigorous reaction condition such as acidic environment pH ranging from 2 to 4.5 so that the mildly acidic character pH between 6.5 and 6.9 in TME cannot effectively initiate the reaction at a high degree [14, 15]. Taken together, effective TME regulation including eliminating intratumoral GSH, elevating endogenous H$_2$O$_2$ level and increasing acidity is clinically urgent to develop efficient strategies to improve the catalytic performance for CDT [16, 17].

On the basis of Warburg effect, the proliferating cancer cells consume much more nutrients such as glucose than normal cells to meet their own energy demand for cell survival, growth and differentiation. Glucose oxidase (GOD)-mediated metabolism reacts with glucose in TME to produce H$_2$O$_2$ and gluconic acid, which blocks the tumorous energy supply by consuming glucose, thereby starving tumor cells death [18–20]. Furthermore, the generated H$_2$O$_2$ provides abundant reactants for CDT, meanwhile accompanying with generated gluconic acid for inducing more acidic environment, consequently improving the therapeutic efficiency of CDT [21, 22]. Moreover, it has been proven that when the temperature achieves at 50 °C, the catalytic activity of GOD reaches its maximum. Photothermal therapy (PTT) employing photothermal agents (PTAs) converts the near-infrared (NIR) light energy into heat energy in target region for ablating tumors [23]. Notably, compared with the traditional first near-infrared (NIR-I) biological window 650–950 nm, the second near-infrared (NIR-II) biological window 1000–1350 nm possesses several remarkable advantages, such as deeper penetration of biological tissues and less tissue scattering and absorption. Although great efforts have been devoted to exploring and developing PTAs including plasmonic metals (e.g., palladium nanosheets, gold nanostructures) [24, 25], transition metal dichalcogenides and oxides [26, 27], two-dimensional (2D) metal carbides and nitrides (MXenes, e.g., Ti$_3$C$_2$, Nb$_2$C, Mo$_2$C, V$_2$C, Ta$_3$C$_4$ and W$_{1.33}$C) [28–31], 2D monoelement materials (Xenes, e.g., siliconene, germanene, phosphorene, arsenene, antimonene, bismuthene) [32, 33], and conjugated polymers [34, 35], some critical issues are still required to be addressed. The non-specificity, reduced therapeutic efficacy, unclear long-term biological consequences and off-target heating-induced noncancerous regions damage are Gordian knots for current PTAs. Therefore, improving the accumulation of PTAs in tumor tissues based on TME is one of the most desirable strategies for efficient tumor treatment.

In this work, we have designed and engineered a kind of intelligent molybdenum (Mo)-based polyoxometalate (POM) nanoclusters modified with GOD (GOD@POMs) as a multifunctional therapeutic catalytic nanosystem based on the strategy of photonic hyperthermia-reinforced and specific TME-triggered cascaded nanocatalytic cancer treatment (Scheme 1). When these multifunctional GOD@POMs enter the tumor region, GOD serves as the start point to deplete glucose for blocking the nutrients/energy supply to tumor cells. Furthermore, the post-produced H$_2$O$_2$ could oxidize the Mo (V) into Mo (VI) that results in the efficient formation...
of cytotoxic singlet oxygen ($^1{\text{O}_2}$) on the basis of Russell mechanism, which is unlike traditional Fenton-like agents (Fe, Cu and Mn) that generate noxious hydroxyl radicals (${\cdot}\text{OH}$), and the Mo (VI) could consume GSH to form Mo(V). Meanwhile, compared to other PTAs, pH-responsive Mo-based POM may aggregate from small nanoparticle to big ones in mildly acidic tumors, enabling the tumor-specific targeting therapy and enhancing the photothermal conversion. Thus, the decreased pH in TME resulting from the formed gluconic acid promotes the self-assembly and self-adaptive photothermal conversion of Mo-based POM, which could serve as a desirable NIR-II PTAs. Under the NIR-II laser irradiation, the light-to-heat conversion capacity of POM elevates the local temperature, achieving efficient PTT, which not only improves the catalytic efficiency of GOD but also promotes the ROS generation during the Mo-mediated CDT process. This rationally engineered multifunctional nanosystem provides a distinct paradigm of collaborative treatment strategy to achieve highly efficient tumor treatment with desirable clinical translation prospects.

**Materials and methods**

**Materials and reagents**

Molybdenum carbide (Mo$_2$C), 3-aminopropyltriethoxysilane (APTES), glucose oxidase (GOD), N-(3-Dimethylaminopropyl)-N’-ethylcarbodiimide hydrochloride (EDC), N-hydroxyl succinimide (NHS), hydrogen peroxide (H$_2$O$_2$), hydrochloric acid (HCl), 1,3-diphenylisobenzofuran (DPBF), 2,7-dichlorofluorescein diacetate (DCFH-DA) and glucose were obtained from Sigma-Aldrich Trading Co., Ltd. (Shanghai, China). Cell
counting kit-8 (CCK-8), calcein-AM and propidium iodide (PI) were purchased from Beyotime Biotechnology (Shanghai, China). Dulbecco’s modified Eagle medium (DMEM), fetal bovine serum (FBS), penicillin-streptomycin solution, phosphate buffer saline (PBS), and trypsin were purchased from Gibco Trading Co., Ltd. (Shanghai, China). All chemicals were used as received unless otherwise stated.

Synthesis of polyoxometalate (POM)
The POM was synthesized from bulk Mo2C powders via one-pot oxidation reaction. 2 g Mo2C powder was dispersed in 15 mL deionized (DI) water with vigorous stirring. Then, 2 mL H2O2 was added drop by drop and the reaction was kept overnight. When the reaction was finished, Mo2C residue was removed by centrifugation (3000 rpm). After lyophilization, deep blue colored powder was obtained as Mo-based POM.

Synthesis of polyoxometalate-amino (POM-NH2)
1.8 mg/mL POM aqueous solution was slowly added in 0.37 mL APTES. After the solution became clear, its pH was adjusted to 1.5 with 1 M HCl solution. The solution was then vigorously stirred for 24 h, and the precipitate was obtained by 10,000 rpm centrifugation. Finally, the precipitate was collected and washed with DI water, and dispersed in 2.5 mL DI water for further use.

Synthesis of GOD@POMs
38 mg EDC, 57 mg NHS and 0.5 mg GOD were dissolved in 6 mL DI water followed by adding 1 mL POM-NH2 dispersion. The system was stirred for 8 h at room temperature to produce GOD@POMs. After centrifugation, the precipitate was collected and washed with DI water, and dispersed in 2.5 mL DI water for further use.

Characterization
Morphologies were characterized using a SU8010 field emission scanning electron microscope (SEM, Hitachi, Japan) and transmission electron microscope (TEM, JEOL JEM-2100plus). Dynamic particle size was measured on a Zetasizer Nanoseries (Nano ZS90, Malvern Instrument Ltd.). Ultraviolet-visible-near-infrared (UV–vis–NIR) absorption spectrum was recorded using a Shimadzu UV3600 UV–vis–NIR scanning spectrometer (Shimadzu Scientific Instruments, Japan). Fourier transform infrared (FTIR) spectroscopy were collected with a Thermo Scientific™ Nicolet™ iS5 FTIR analyzer. GOD encapsulation was determined by Netzsch TG 209 F3 Tarsus. X-ray photoelectron spectroscopy (XPS) measurements were carried out on the Thermal Scientific™ K-Alpha™.

Solution stabilities of GOD@POMs
GOD@POMs (Mo concentration: 1000 μmol/L) were dispersed in H2O and PBS respectively. After that, we recorded its absorption by UV-vis-NIR and took digital photos at 24 and 72 h respectively.

Measurement of pH changes
After adding 1, 2 or 3 mg/mL glucose into GOD@POMs aqueous solution with same Mo concentration (1000 μmol/L), pH of each system was measured at an interval of 30 s, and the whole reaction process was kept for 300 s.

Quantitative analysis of the $^{1}\text{O}_2$ generation
DPBF was applied as a probe to detect the generation of $^{1}\text{O}_2$ in GOD@POMs dispersion with existence of H2O2 and glucose. Firstly, GOD@POMs aqueous solution (Mo concentration: 1000 μmol/L) mixed with DPBF (1 mg/mL, dissolved in DMF), and then the test started when adding H2O2 (10 mM) or glucose (1 mg/mL) into the mixed solution. For the reaction between GOD@POMs and H2O2, the absorbance of DPBF at 420 nm was recorded every 2 min using UV–vis–NIR spectra. For the reaction between GOD@POMs and glucose, the absorbance of DPBF at 420 nm was recorded every 5 min.

Photothermal performance of GOD@POMs
UV absorption of GOD@POMs with different Mo concentration (0, 250, 500, 750, 1000 and 1500 μmol/L) was detected. To record temperature-changes curves, GOD@POMs aqueous solutions with different Mo concentration (0, 250, 500, 750 and 1000 μmol/L) were adopted under NIR-II laser irradiation at different power densities (0.5, 0.8, 1.0 and 1.5 W/cm²) for 10 min. Subsequently, in order to evaluate the photothermal stability of GOD@POMs, temperature changes of GOD@POMs solution (Mo concentration: 1000 μmol/L) through five laser on/off cycles (1 W/cm²) were recorded.

Cell culture
The mouse fibroblast cell line (L929 cells) is applied for cytotoxicity assessments. The C6 rat glioma cell line is used as a cell model for neurological tumor. Both the L929 mouse fibroblasts cell line and C6 rat glioma cell line was obtained from the Cell Bank of Shanghai Institutes for Biological Sciences, Chinese Academy of Sciences (Shanghai, China). All cells were regularly maintained in complete DMEM medium supplemented 10% FBS, 100 U/mL penicillin and 100 U/mL streptomycin and kept at 37°C in a humidified atmosphere of 5% CO2 and 95% air. The medium was changed every two days, and the cells were routinely passaged by using 0.25% trypsin solution before approaching 80% confluence.
Cell endocytosis of GOD@POMs
To confirm the endocytosis of GOD@POMs, fluorescein isothiocyanate (FITC) was applied to label GOD@POMs. C6 cells were seeded in confocal dishes and then incubated with FITC-labelled GOD@POMs. After co-incubation for 0 and 8 h, confocal laser scanning microscopy (CLSM) was used to detect cell endocytosis.

In vitro cytotoxicity of GOD@POMs
To assess the cytotoxicity of GOD@POMs, L929 cells were seeded into a 96-well plate with the density of $1 \times 10^4$ cells per well and then cultured at 37 °C for 24 h. Then, GOD@POMs dispersion were added into the wells and co-incubated for another 24 h. At the end of co-incubation, 100 μL 10-fold diluted CCK-8 were added into each well. After co-incubation for another 4 h, the absorbance of CCK-8 was monitored by a micro-plate reader at the wavelength of 450 nm.

In vitro anti-tumor assessment
To verify the effects of reaction between GOD and glucose, glucose (25, 50, 100, 125 and 250 μg/mL) were reacted with GOD@POMs or POMs (Mo concentration: 1000 μmol/L) and then the standard CCK-8 assay was performed to access the cell viability. Besides, to test the photothermal ablation performance, C6 cells were seeded into a 96-well plate with the density of $1 \times 10^4$ cells per well and then cultured overnight. Then, the C6 cells were incubated GOD@POMs or POMs with different Mo concentration (0, 250, 500, 750, 1000 and 1500 μmol/L). After 4 h incubation, the cells were exposed to the 1064 nm laser irradiation (1 W/cm², 5 min). After that, the cell viabilities were measured by CCK-8 assay to compare the therapeutic effects of different treatments: (I) Control; (II) Laser; (III) GOD@POMs; (IV) GOD@POMs + Laser; (V) GOD@POMs + Glucose; (VI) GOD@POMs + Laser + Glucose. The Mo concentration of GOD@POMs was 1000 μmol/L and the concentration of glucose was 1 mg/mL. The condition of 1064 nm laser treatment was irradiated at the power density of 1 W/cm² for 5 min. After that, the cells were washed three times by PBS. Finally, the intracellular ROS generation was determined by CLSM. Flow cytometry was also used to quantitatively detect ROS generation. C6 cells were seeded into 6-well plates, and then the DCFH-DA was added and co-incubated for 30 min. Finally, cells were treated with previous manners and then collected to detect the ROS by flow cytometry.

Animals and treatment
Six-week-old healthy female Kunming mice and thirty BALB/C nude mice with 4–6 weeks were purchased from Slac Laboratory Animal Co., Ltd. (Shanghai, China). The animals were housed in stainless steel and ventilated cages under the standard conditions (temperature: 25 ± 2 °C, relative humidity: 60 ± 10%, and light: 12 h light/dark cycle) for seven days prior to treatment. All animal experiments were performed with the approval of the ethics by the Ethics Committee of Shanghai University (License number: ECSHU-2021-029).

Photoacoustic (PA) imaging
Different Mo concentrations of GOD@POMs (250, 500, 750, 1000 and 1500 μmol/L) dissolved in purified water were performed with excitation wavelength of 808 nm and 1200 nm. For PA imaging in vivo, the C6 tumor bearing mice were intravenously injected with GOD@POMs (10 mg/kg). After the injection, the signal was recorded with excitation wavelength at 1200 nm.
In vivo IR-thermal imaging
To verify the NIR-II laser-triggered tumor hyperthermia, C6 tumor bearing mice were intravenously injected with GOD@POMs (10 mg/kg). At 6 h post-injection, the tumors were irradiated with 1064 nm laser (1 W/cm², 10 min). The photothermal heating curves and photothermal heating images of tumors at 0, 2, 4, 6, 8 and 10 min were recorded.

In vivo toxicity assessment of GOD@POMs
Ten Kunming mice were assigned to two groups, which were intravenously injected with GOD@POMs (10 mg/kg), and mice injected with PBS were set as the control group. The body weight of the mice was measured every other day. The mice were anesthetized and dissected in 28 days of post-injection. The blood was taken out for blood routine and blood biochemical analysis. The major organs (heart, liver, spleen, lung and kidney) were dissected, fixed in a 10% formalin solution and stained with hematoxylin and eosin (H&E) for histological analysis.

In vivo biodistribution
A C6 tumor-bearing model was established by subcutaneous inoculation of C6 cells (1 × 10⁶) on the right leg of BALB/C nude mice. To assess the in vivo biodistribution, Cyanine 5.5 (Cy5.5) was initially used to label GOD@POMs and then the in vivo fluorescence distribution at different time intervals were monitored by using in vivo imaging system (IVIS). After that, the mice were euthanized followed by collecting the organs including heart, liver, spleen, lung, kidney and tumors. The ex vivo fluorescent images were acquired.

In vivo tumor therapy
Thirty C6 tumor bearing BALB/C nude mice were divided into six groups (n = 5 in each group): (I) Control; (II) Laser; (III) GOD; (IV) POMs; (V) GOD@POMs; (VI) GOD@POMs + Laser. For control group, the tumor-bearing mice were merely injected with PBS. For GOD and POMs group, the mice were injected with only GOD or only POMs. For GOD@POMs and GOD@POMs + Laser group, the mice were injected with GOD@POMs (10 mg/kg). Further, Laser and GOD@POMs + Laser groups were irradiated with 1064 nm laser at the power density of 1 W/cm² for 10 min at 6 h post-injection, and the tumor temperature was monitored by IR camera. The tumor volume and body weight were recorded every other day. After 15 days of treatment, all mice were sacrificed, and the main organ tissues of each group of mice were dissected for H&E histological analysis, TdT-mediated dUTP nick end labeling (TUNEL) and Ki-67 antibody staining to observe cell apoptosis and cell proliferation. Tumor volume was calculated by following equation: \( V = \text{length} \times \text{width}^2 \times 0.5 \), where length and width denote the maximum length and maximum width of the tumor of the mice.

Results
Synthesis and characterizations of GOD@POMs
For the successful synthesis of Mo-based POMs, Mo₃C powder was reacted with H₂O₂ in a facile one-pot procedure. As shown in the TEM images, the obtained POMs possess a spherical structure (Fig. 1a). Subsequently, for the GOD grafting, the POMs were reacted with APTES to generate amino groups onto the surface, termed as POM-NH₂ (Fig. 1a), the average diameter of which is 215 nm, and then covalently conjugated with the carboxyl of GOD through amide bond via EDC/NHS coupling, defined as GOD@POMs. Next, TEM images show that GOD@POMs feature spherical shape and the average diameter is around 255 nm (Fig. 1a, b). Besides, the zeta potential slightly increases from POMs (−35.5 mV) to POM-NH₂ (−29.0 mV) to GOD@POMs (−25.8 mV), which originates from the surface GOD modification (Fig. 1c). FTIR spectroscopy analysis indicates the vibration bands at 3300–3500 cm⁻¹ region related to the stretching vibration of -NH₂ and the band centered at 1650 cm⁻¹ ascribed to the stretching vibration of C=O (Fig. 1d), confirming the successful surface conjugation of GOD. Notably, the loading amount of GOD is tested and calculated to be 10.0 wt% according to the thermogravimetric analysis (TGA) results (Fig. S1, Supporting Information). The UV-vis-NIR absorption spectrum of GOD@POMs exhibits broad and intense absorption in NIR region, especially in NIR-II biowindow, which indicates their high potential to serve as the desirable photothermal agent (Fig. 1e). In addition, XPS spectra of the elements O, N, C, and Mo further demonstrate the desirable synthesis of GOD@POMs (Fig. 1f). Especially, the Mo element in POMs displays mixed valence states containing Mo⁵⁺ and Mo⁶⁺ on the 3d orbit (Fig. 1g). Following amino group and GOD surface modification, the mixed valence states of Mo in POM-NH₂ and GOD@POMs reveal neglectable change. Through the observation of UV-vis-NIR, the absorbance of GOD@POMs exhibits neglectable changes with the prolongation of time, no matter it was dispersed in water or in PBS, indicating that it features preferable solution stability (Fig. S2, Supporting Information).

Catalytic and photothermal performance of GOD@POMs
Given that GOD can efficiently catalyze glucose into gluconic acid and H₂O₂, the GOD@POMs were reacted with glucose to testify the catalytic activity of conjugated GOD. The results indicate that the generated gluconic
acid induces a significant decrease in pH value, which is in a glucose concentration-dependent manner (Fig. 2a). Notably, after treatment with glucose and the decrease of pH induced by generated gluconic acid, the TEM images graphically reveal the aggregation of POMs in acidic environments, showing TME-specific accumulation (Fig. S3, Supporting Information). Besides, under the same concentration, the blue color of GOD@POMs dispersion deepens monotonically in acidic environment, corresponding to the significantly elevated UV-vis-NIR absorption (Fig. S4, Supporting Information). Subsequently, DPBF was applied to detect $^1\text{O}_2$ generation capability of GOD@POMs. As the $\text{H}_2\text{O}_2$ co-reaction time prolonged, the characteristic absorption peak of DPBF at 420 nm significantly decreased (Fig. 2b), indicating the substantial $^1\text{O}_2$ production. Furthermore, once the addition of glucose, the absorption peak of DPBF decreases in both time-dependent and glucose concentration-dependent manners (Fig. 2c, Fig. S5, Supporting Information), which is attributed to the presence of GOD in GOD@POMs catalyzing the oxidation of glucose into $\text{H}_2\text{O}_2$, thus initiating a cascade catalytic reaction for $^1\text{O}_2$ generation.

In addition, the UV-vis-NIR absorption spectra reveals that GOD@POMs feature wide and strong absorption
covering both the NIR-I and NIR-II biological window (Fig. 2d), elucidating the strong NIR laser absorption ability of GOD@POMs, following a concentration-dependent manner. Then, the photothermal performance of GOD@POMs was assessed. As expected, after exposure to 1064 nm laser irradiation, the temperature of GOD@POMs aqueous solution remarkably rises in a power density-dependent and concentration-dependent way (Fig. 2e, f and i), and the temperature can reach 50.7°C when Mo concentration is 1000 μmol/L under 1064 nm laser irradiation at 1.5 W/cm² for 10 min. The photothermal-conversion efficiency of GOD@POMs is calculated to be 48.1% at 1064 nm (Fig. 2g, Fig. S6 Supporting Information), surpassing most available photothermal agents such as MnSe2@PVP (39.1%) (Table S1). In addition, almost no apparent deterioration can be detected during the five successive laser on/off cycles, confirming the impressive photothermal stability of GOD@POMs (Fig. 2h).
In vitro photothermal-enhanced cascade catalytic therapy

The cellular uptake of C6 cells towards GOD@POMs was performed to uncover their internalization behaviour. To verify the cellular uptake of GOD@POMs, the FITC-labelled GOD@POMs were incubated with C6 cells. After 8 h co-incubation, the stronger green fluorescence intensity can be clearly observed, which indicates that the GOD@POMs can be effectively internalized by the endocytic pathway (Fig. S7, Supporting Information). Prior to investigating the anti-cancer effects of GOD@POMs in vitro, the cytotoxicity of GOD@POMs was initially assessed on L929 murine fibroblast cell line using standard CCK-8 assay. After co-incubation at various Mo concentrations for 24 h, GOD@POMs exhibit no obvious cytotoxicity to L929 cells, and the cell viability is still above 80% even exposure to nanoparticles at the Mo concentration of as high as 2000 μmol/L (Fig. S8, Supporting Information), indicating that GOD@POMs possess low toxicity to normal cells. Subsequently, the in vitro therapeutic efficacy of GOD@POMs was evaluated on C6 rat glioma cell line. As shown in Fig. 3a, compared to glucose only group and POMs + Glucose group which exhibit no obvious cell-killing abilities, with the glucose concentration increasing from 0 to 250 μg/mL, the cell viability of GOD@POMs + Glucose group declines significantly from 100 to 35.7%, revealing that GOD@POMs react with glucose to produce ROS for cell killing through cascade catalytic reaction. Moreover, under 1064 nm laser irradiation, in contrast to only 43.4% of apoptotic cells in the POMs group, GOD@POMs induce up to 63.1% C6 cell death at the Mo concentration of 1500 μmol/L, which is lower than the group without laser irradiation and POMs + Laser group. The superior cell killing of GOD@POMs under laser irradiation is owing to the acidity environment enhanced by generated gluconic acid, making the POMs aggregate and resulting stronger hyperthermia effects (Fig. 3b, Fig. S9, Supporting Information).

To further confirm the synergistic therapy effect, C6 cells were divided into six groups: (I) Control; (II) Laser (1 W/cm², 5 min); (III) GOD@POMs; (IV) GOD@POMs + Laser (1 W/cm², 5 min); (V) GOD@POMs + Glucose; (VI) GOD@POMs + Glucose + Laser (1 W/cm², 5 min). Comparatively, there are 52.0% and 54.5% cells survived in the GOD@POMs + Laser group and GOD@POMs + Glucose group, respectively, while only 38.69% of C6 cells survived in the GOD@POMs + Glucose + Laser group, verifying the synergistic anti-cancer effect in vitro (Fig. 3c).

Furthermore, the killing effect after different treatments is detected by co-staining with calcein AM (green, live cells) and propidium iodide (PI, red, dead cells) (Fig. 3d). The results show that, compared with the groups without glucose, GOD@POMs + Glucose group and GOD@POMs + Laser group display strong red fluorescence from PI, resulting from the GOD-induced starvation therapy by glucose consumption following the H2O2 generation-facilitated Mo-based CDT. Moreover, there is almost no green fluorescence from calcein AM in GOD@POMs + Glucose + Laser group, which is ascribed to the PTT and meanwhile the photonic hyperthermia-promoted cascade catalytic reaction, achieving synergistic therapy. Corresponding to the results of CLSM images, the flow cytometry apoptosis assay exhibits that the GOD@POMs + Glucose + Laser group causes the maximum amounts of total 47.48% cell apoptosis (Fig. 3e). Moreover, in order to explore the intracellular mechanism mainly depending on the ROS, DCFH-DA as a typical ROS fluorescent probe was used (Fig. 3f). Compared with GOD@POMs group, C6 cells in GOD@POMs + Glucose group exhibit enhanced green fluorescence by CLSM images and flow cytometry analysis, which indicates that GOD@POMs react with glucose to yield ROS. Besides, the cells after treatment with GOD@POM + Glucose + Laser display the strongest green fluorescence, suggesting that the hyperthermia can accelerate the ROS generation (Fig. 3g).

In vivo anti-tumor effect of GOD@POMs on the C6 tumor-bearing mice

Considering that the biosafety is the first priority for the biomedical application, we systematically studied the biocompatibility and biodistribution of GOD@POMs in vivo. The Kunming mice were intravenously injected with GOD@POMs and the blood and main organs were collected including heart, liver, spleen, lung and kidney for biosafety assessment. During the 4 weeks observation, compared with control group, no significant difference in body weight is monitored in the mice after treatment with GOD@POMs (Fig. S10, Supporting Information). Besides, after administration with GOD@POMs, the blood routine is distributed within the normal range, suggesting that GOD@POMs induce no side effects to the mice (Fig. S11, Supporting Information). Additionally, almost no obvious pathological abnormality is observed in the GOD@POMs.
Fig. 3 (See legend on previous page.)
group (Fig. S12, Supporting Information). All these in vivo evaluation data strongly demonstrate the desireable biosafety of the engineered multifunctional GOD@POMs nanosystem.

To evaluate the in vivo behaviors, Cy5.5 labelled GOD@POMs were fabricated for biodistribution and tumor accumulation study using fluorescent imaging. As shown in Fig. S13a and S13b, the fluorescence intensity of the tumor gradually increases and reaches the peak after 4 h, indicating the efficient tumor uptake of GOD@POMs. At the following time points, the fluorescence signals slowly decrease. Moreover, the ex vivo fluorescence images and corresponding fluorescent intensity illustrate that the GOD@POMs could efficiently accumulate in the tumor and clear from other organs. (Fig. S13c-d, Supporting Information).

Inspired by the excellent therapeutic effects in vitro, the satisfactory biosafety in vivo and efficient tumor accumulation, we further investigated the anti-tumor efficacy of GOD@POMs on C6 tumor-bearing BALB/C nude mice. Since GOD@POMs possess the strong absorption in both NIR-I and NIR-II regions, they can serve as a potential contrast agent for PA imaging in vivo. Expectably, with the increased Mo concentration, the PA signals are gradually enhanced in NIR biological window, especially in NIR-II (Fig. S14, Supporting Information). After intravenous injection of GOD@POMs, apparent PA signals are observed in the tumor site, which illustrates that GOD@POMs not only can act as a remarkable contrast-enhanced NIR-II PA agent but also can effectively gather at tumor site through the typical enhanced permeability and retention (EPR) effect (Fig. 4a). Subsequently, all C6-tumor-bearing mice were randomly divided into 6 groups: (I) Control, (II) Laser, (III) GOD, (IV) POMs, (V) GOD@POMs and (VI) GOD@POMs + Laser, in which the mice in group (II) and (VI) are irradiated with 1064 nm laser (1 W/cm²) for 10 min after GOD@POMs injection (Fig. 4b). As shown in Fig. 4c, the temperature of tumor in GOD@POMs + Laser group quickly increases 8°C within 10 minutes, whereas the temperature in laser alone group no significant increase (Fig. 4d), which manifests the benign photothermal performance of GOD@POMs. During the treatment process, the mice weight and tumor volume are recorded every 2 days. Compared with the control group, GOD@POMs group exhibits a certain tumor growth inhibition ratio of 50% owing to the GOD-mediated starvation therapy combined with POM-based CDT. Important, it is found that the tumor growth decreases to only 20% in GOD@POMs + Laser group, confirming that PTT can further improve therapeutic effects (Fig. 4e, f). The mice in each group shows negligible change in body weight, demonstrating almost no adverse effects during the treatment (Fig. 4g).

Subsequently, the tumor sections of each group are stained with the H&E histological analysis, Ki67 and TUNEL antibody staining for pathological evaluation. In accordance with relative tumor volume curves, GOD@POMs + Laser group shows the most significant cell necrosis or damage, in which large areas of tumor cells appear nuclear solid fragmentation and pale red cytoplasm in H&E staining. The results are further confirmed by a large number of apoptotic tumor cells in GOD@POMs + Laser group stained by TUNEL and the obviously reduced proliferation of tumor cells stained by Ki-67 (Fig. 4h). Additionally, in each group, there is no obvious damage or inflammation in H&E staining image of major tissues (e.g., heart, liver, spleen, lung and kidney) (Fig. S15, Supporting Information), suggesting the high therapeutic biosafety of GOD@POMs during the treatment.

**RNA sequencing and analysis of C6 tumor-bearing mice administrated with GOD@POMs under NIR-II laser irradiation**

To further investigate the underlying mechanism of GOD@POMs-mediated synergistic antitumor effect, the typical RNA sequencing (RNaseq) was carried out. As shown in volcano plot, compared with control group, there are 1562 differentially expressed genes, including 1262 up-regulated genes and 300 down-regulated genes (Fig. 5a). Among them, apoptosis-related genes, such as Casp6, Bak1 and Casp8 are up-regulated, suggesting that the GOD@POMs + laser treatment could cause cancer cells apoptosis (Fig. 5b). Meanwhile, the up-regulated expression of genes, including Maob, Sord, Steap3 and Gpx8 are associated with oxidative stress, illustrating that the produced ROS plays an important role in tumor growth inhibition (Fig. 5b).

Subsequently, in order to understand the biological processes and molecular metabolic pathways, Gene Ontology (GO) analysis and Kyoto Encyclopedia of Genes and Genomes (KEGG) pathway analysis were performed to analyze the genes set enrichment. GO analysis indicates that up-regulated genes in GOD@POMs + laser group are related to the regulation of tumor necrosis (Fig. 5c). In addition, after GOD@POMs + laser treatment, KEGG analysis shows that differentially expressed genes are concentrated in pathways associated with apoptosis, tumor necrosis factor (TNF) and mitogen-activated protein kinase (MAPK) signaling pathway (Fig. 5d). Therefore, the RNA sequencing data further demonstrates that the GOD@POMs + laser treatment produces anti-tumor effects associating with tumor apoptosis and necrosis.
Discussion
Compared with normal cells, cancer cells prefer to utilize aerobic glycolysis rather than oxidative phosphorylation for adenosine triphosphate (ATP) production, inducing an increased glucose import to satisfy their rapid proliferation and energy demand. Accordingly, starvation therapy is developed as an effective strategy to suppress tumor growth by blocking glucose supply. GOD, as an endogenous oxido-reductase, can efficiently catalyze glucose into H$_2$O$_2$ and gluconic acid in the presence of molecular oxygen thereby depriving glucose and increasing acidity as well as H$_2$O$_2$ content in TME. The overproduced H$_2$O$_2$, not only trigger oxidative stress but also can be applied as the substrate of Fenton/Fenton-like reaction for ROS generation. Unlike traditional Fenton/Fenton-like agents, based on the specific electronic structure, Mo-based POM is sensitive to [Image 4]
the stimulus of pH and redox environment such as GSH. Mo (VI) to Mo (V) reduction with the help of GSH renders 1O2 production catalyzing H2O2 decomposition through Russell mechanism [36].

In this study, we engineered a tumor-specific catalytic nanosystem GOD@POMs realizing PTT-augmented synergistic starvation combined with CDT. On the basis of POM-mediated CDT and acid-induced aggregation for PTT, the GOD-mediated glucose consumption can realize H2O2 self-supply and more acidic TME, which further promote CDT and PTT process. Moreover, the increased temperature caused by PTT can elevate the

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**Fig. 5**

- **a** Volcano plot of differentially regulated genes between control group and GOD@POMs + laser group.
- **b** Heat-map of differentially expressed genes associated with apoptosis and oxidative stress.
- **c** GO enrichment analysis of the different genes after the GOD@POMs + laser treatment.
- **d** KEGG pathway enrichment analysis based on RNAseq after the GOD@POMs + laser treatment.
reaction activity of GOD, thus building a paradigm for interlocking synergistic anti-tumor pattern.

In spite of the therapeutic effect of GOD@POMs is only preliminarily evaluated on C6 cancer cell and C6 derived cell line xenograft (CDX) model, our work has suggested that GOD@POMs can substantially inhibit tumor growth. In the future, it will be interesting to test whether it can be extended to other tumor models or patient derived xenograft (PDX) to comprehensively prove its anti-tumor effect and clinical transformation potential. Additionally, only Mo-based POM is used to covalently connect GOD in current experiment, and it is also worth further exploring whether GOD or other endogenous oxido-reductase could be combined with other pre-transition metal-based POMs such as vanadium, tungsten and so on to produce similar effects, which will broaden the application of POM in biomedical industry.

Conclusions

In summary, we have successfully designed and engineered a highly synergistic therapeutic nanoplatform GOD@POMs by elaborately grafting GOD onto POM. GOD catalyzes the oxidation of intratumor glucose into gluconic acid and H₂O₂, which not only blocks the tumor energy supply for starvation therapy, but also elevates H₂O₂ level for subsequent CDT. Furthermore, the redox reaction between Mo (VI) sites and Mo(V) active sites on POM leads to GSH depletion and then trigger the self-supply H₂O₂ to yield abundant ¹O₂ by Mediated Russell reaction. Meanwhile, the decreased pH in TME resulting from the produced gluconic acid promotes the aggregation of Mo-based POM, which can act as NIR-II PTAs for PA imaging-guided photonic tumor hyperthermia, further augmenting the nanocatalytic tumor-therapeutic efficacy. This specific tumor-specific nanocatalytic paradigm represents the desirable tumor treatment modality with concurrently high therapeutic efficacy and biosafety.

Abbreviations

CDT: Chemodynamic therapy; POM: Polyoxometalate; H₂O₂: Hydrogen peroxide; ROS: Reactive oxygen species; TME: Tumor microenvironment; GSH: Glutathione; GOD: Glucose oxidase; PTT: Photothermal therapy; PTAs: Photothermal agents; NIR: Near-infrared; PA: Photoacoustic; ¹O₂: Singlet oxygen; APTES: 3-aminopropyltriethoxysilane; EDC: 1-(3-Dimethylaminopropyl)-3-ethylcarboxydimide hydrochloride; NHS: N-Hydroxy succinimide; DPBF: 1, 3-diphenylisobenzofuran; DCFH-DA: 2,7-dichlorofluorescein diacetate; FBS: Fetal bovine serum; PBS: Phosphate buffer saline; SEM: Scanning electron microscope; TEM: Transmission electron microscope; UV-vis-NIR: Ultraviolet-visible-near-infrared; FTIR: Fourier transform infrared; XPS: X-ray photoelectron spectroscopy; TGA: Thermogravimetric analysis; EPR: Enhanced permeability and retention effect; CCK-8: Cell counting kit-8; H&E: hematoxylin and eosin.

Supplementary Information

The online version contains supplementary material available at https://doi.org/10.1186/s40824-022-00317-y.

Additional file 1: Fig. S1. TG analysis of POMs, POM-NH₂, and GOD@POMs. Fig. S2. UV-vis-NIR absorption of GOD@POMs dispersed in H₂O or PBS at 24 h and 72 h. Fig. S3. TEM image of aggregated GOD@POMs after reaction with glucose. Fig. S4. UV-vis-NIR spectra and the corresponding digital photo of GOD@POMs dispersed in PBS with different pH values ranging from 4.0 to 7.3. Fig. S5. Glucose concentration and time-dependent oxidation of DPBF by GOD@POMs. Fig. S6. Heating and cooling curve of GOD@POMs aqueous solution under 1064 nm laser irradiation at 1.0W/cm². Fig. S7. CLSM images of C6 cells incubated with FITC-labelled GOD@POM after 8 h. Fig. S8. Cell viability assay of L929 cells after treatment with GOD@POMs 24 h at various concentrations. Fig. S9. Cell viabilities of C6 cells after treatment with POMs at various concentrations with or without laser irradiation (1064 nm, 1 W/cm², 5 min). Fig. S10. The body weight of Kunming mice during 28 days observation after different treatments. Fig. S11. Biosafety evaluations of GOD@POMs in vivo. Fig. S12. H&E staining of major organ including heart, liver, spleen, lung and kidney collected from Kunming mice after 28 days treatment. Scale bar: 100 μm.

Fig. S13. (a) Representative in vivo fluorescence images of C6 tumor-bearing mice at 0, 2, 4, 6, 8 and 12h after intravenous injection of GOD@POMs. (b) Quantitative ROI assays of the fluorescence intensity of tumor at designated time points. (c) Ex vivo fluorescence images of major organs at 12 and 24 h after intravenous injection of GOD@POMs (H: heart, Li: liver, Sp: spleen, Lu: lung, Ki: kidney, Tu: tumor). (d) Quantitative ROI assays of the ex vivo fluorescence intensity of major organs and tumors. Fig. S14. In vivo NIR-I and NIR-II PA images of GOD@POMs at various Mo concentration (250, 500, 750, 1000 and 1500 μmol/L). Fig. S15. H&E staining of major organ tissues collected from mice after different treatments Scale bar: 100 μm. Table S1. The light-to-heat conversion efficiency of different of photothermal agents in the reported literatures.

Acknowledgements

Not applicable.

Authors’ contributions

SZ is responsible for the experimental operations. JX is responsible for writing of the manuscript. YD is responsible for data processing. WF is responsible for images generation. LC is responsible for the instruction of experiment. YW is responsible for the experimental design. XN and YC are responsible for the revision of the manuscript. All authors read and approved the final manuscript.

Funding

This work was financially supported by National Natural Science Foundation of China (Grant No. S2072393 and S2272279), Basic Research Program of Shanghai Municipal Government (Grant No. 21JC1406002), International Collaboration Project of Chinese Academy of Sciences (Grant No. GHJZ2072), Shanghai Science and Technology Committee Rising-Star Program (Grant No. 21Q14103100), Nantong Science and Technology Program (Grant No. MS120211100), Shanghai Science and Technology Program (Grant No. 21010000100).

Availability of data and materials

The data and analysis generated in this study are included in articles and supplementary information files.

Declarations

Ethics approval and consent to participate

All animal experiments were performed with the approval of the ethics by the Ethics Committee of Shanghai University (License number: ECSHU-2021-029).

Consent for publication

All authors agreed to publish this manuscript.
Competing interests
The authors declare no conflict of interest.

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Received: 25 July 2022   Accepted: 8 November 2022
Published online: 26 November 2022

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