Unconscious learning of auditory discrimination using mismatch negativity (MMN) neurofeedback

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Neurofeedback is a strong direct training method for brain function, wherein brain activity patterns are measured and displayed as feedback, and trainees try to stabilize the feedback signal onto certain desirable states to regulate their own mental states. Here, we introduce a novel neurofeedback method, using the mismatch negativity (MMN) responses elicited by similar sounds that cannot be consciously discriminated. Through neurofeedback training, without participants’ attention to the auditory stimuli or awareness of what was to be learned, we found that the participants could unconsciously achieve a significant improvement in the auditory discrimination of the applied stimuli. Our method has great potential to provide effortless auditory perceptual training. Based on this method, participants do not need to make an effort to discriminate auditory stimuli, and can choose tasks of interest without boredom due to training. In particular, it could be used to train people to recognize speech sounds that do not exist in their native language and thereby facilitate foreign language learning.

Perceptual learning often requires a significant amount of training and attention to the training task from the participant, particularly when the learning target cannot be perceived, as in auditory discrimination. It is not explicitly clear what and how to learn effectively. For example, native Japanese speakers are usually unable to perceive the difference between /l/ and /r/ sounds¹⁻⁴ in English, and thus a long duration is required for training. Similarly, much training is needed for native English speakers to discriminate Mandarin tones⁵. This difficulty can be observed in not only language education, but also other fields such as training people with hearing impairments or learning difficulties, musicians, or sound engineers. Although a recent study⁶ indicated that visual perceptual improvement was observed using decoded fMRI neurofeedback without stimulus presentation, this technique requires participants to discriminate the target in advance.

Many previous studies⁷⁻¹¹ have shown that auditory discrimination ability improves with a significant amount of behavioral training, while mismatch negativity (MMN) becomes stronger as an index of sound discrimination accuracy. The MMN can be elicited by any discriminable auditory change, and provides a separate objective measure of the discrimination accuracy for any dimension of auditory stimulation¹²,¹³. Interestingly, the MMN response can be detected in the absence of a conscious realization of the contrast¹⁴. Furthermore, an MMN can be elicited without the listener subjectively attending to the sound stimuli¹⁵,¹⁶.

In this study, we developed a novel neurofeedback method where the strength of participants’ MMN, as a measure of perceptual discriminability, is presented as visual feedback to provide a continuous cue for learning. While focusing on the visual feedback, participants unconsciously achieved a significant improvement in auditory discrimination of the applied stimuli.

Results

In our experiment, the participants were randomly distributed into the neurofeedback (n = 8 : P₁,...,P₈) and control groups (n = 8 : P₉,...,P₁₆) to compare the effect of neurofeedback. The sequences of tones used for the neurofeedback group consisted of a standard stimulus (1000 Hz, 80% of tones) and a deviant stimulus (1008 Hz, 20% of tones). The two stimuli were presented in random order every 0.5 s (Fig. 1a). The average amplitude of the MMNs was calculated from responses to the previous 20 stimuli (16 standard and 4 deviant stimuli) and was represented by a solid green disc, the radius of which corresponded to the amplitude of the MMN (Fig. 1a).
Participants were instructed to ignore the sounds played through their earphones and concentrate on making the solid green disc presented on the screen as large as possible. The radius of the green disc was fixed for the first 20 stimuli of the session, because these 20 sounds are needed to calculate the MMN. Following this, the radius of the disc was determined every 0.5 s by linearly mapping the amplitude of the MMN (see Methods).

**Improvement in the behavioral auditory discrimination (BAD) test.** To evaluate the improvement in participants’ auditory perception, a BAD test was performed before the first day of training (pre-training test) and after each training day. In the BAD test, participants were asked whether two pure tones (the same 1000 Hz and 1008 Hz stimuli that were used for training) were different (Fig. 1b and 1c). Figure 2a shows the performance of all 8 participants in each BAD test. A one-way analysis of variance with repeated measures indicated a significant effect of training ($F(5, 42) = 8.40, P < 0.0001$). A post-hoc t-test comparing accuracies on subsequent training days revealed that the discrimination between the two pure tones significantly improved on all but the 3rd and 4th days ($t(7) = 6.01, P < 0.01$; $t(7) = 5.01, P < 0.05$; and $t(7) = 5.49, P < 0.05$, with Bonferroni correction for the 1st, 2nd and 5th day, respectively). Overall, we found a gradual increase in the discrimination accuracy during each training day, and an increase in the mean discrimination accuracy on subsequent training days (Fig. 2c). There was a significant improvement of 25.45 ± 3.09% (mean ± s.e.m. across participants) in discrimination accuracy on the final day of training when compared with the results of the pre-training test [$t(7) = 8.23, P < 0.001$ with a Bonferroni correction].

Although the participants were asked to ignore the auditory stimuli during training, we hypothesized that they might become accustomed to hearing the stimuli repeatedly, and thus, learning might unconsciously occur and auditory discrimination performance might improve. Furthermore, a previous study in perceptual learning reported that repetitive pairing of reward and visual stimuli leads to performance improvement on that stimuli$^{17}$. Therefore, there is a possibility that the size of the disc had worked as a reinforcement signal and repetitive pairing of this reinforcement signal and auditory stimuli led to the behavioral improvements. To test these possibilities, we performed a control experiment with 8 new participants (control groups: P9,…,P16) who were given the same stimuli and instructions as the neurofeedback group. Electrodes were also attached to the participants, but the sizes of the green discs they were shown did not correspond to their MMN responses. Instead, the sizes corresponded to the sequences of visual stimulus presented to participants in the neurofeedback group. It should be noted that the participants did not know whether they were in the neurofeedback or control group. We measured the performance of each participant in the control group using the BAD test (Fig. 2b). A one-way analysis of variance with repeated measures indicated that there was no significant improvement in performance ($F(5, 42) = 0.16, P = 0.98$; Fig. 2c). Furthermore, Figure. 2c indicates that there was no significant difference in performance on the pre-test between the neurofeedback and control groups. In addition, the score in the pre-test was not significantly different from chance (50% correct), as tested by a binomial test (the critical score of significant difference was 60.6%). However, we found that the average discrimination performance improved significantly in the neurofeedback group compared with the control group ($t(7) = 7.72, P < 0.001$) (Fig. 2d). Taken together, these results demonstrate that the improvement in discrimination performance observed in the neurofeedback group was not attributable simply to repeatedly hearing the sound stimuli (Fig. 2c).

**Improvement in neural activity.** We also assessed whether neural activity changed in the neurofeedback and control groups. Using the electroencephalography (EEG) data collected on each training day, we found that the average MMN amplitude on the last training day was significantly higher when compared with the first training day in
the neurofeedback group (t = 2.45, P = 0.044) (Fig. 3a). In addition, the average daily MMN peak latency was significantly shorter on the last day when compared with the first day in the neurofeedback group (t = 2.88, P = 0.024) (Fig. 3b). Furthermore, all participants in the neurofeedback group showed significant changes in at least one of the neural measures (MMN amplitude or peak latency), whereas no significant changes were observed in either amplitude or latency of MMNs in the control group (see Supplementary Fig. S1 online).

Figure 3c shows the group grand average MMN responses on the 1st and 5th training days in the neurofeedback and control groups, respectively. However, due to the difference in peak latency between participants, the result shown in fig. 3c differs somewhat from fig. 3a and 3b.

Discussion

A recent study has reported that visual perceptual learning can be achieved by inducing activity in the visual cortex that corresponds to orientation detection, using decoded functional magnetic resonance imaging (fMRI) neurofeedback, without stimulus presentation or the participants’ subjective awareness of the aim of learning. Our results support the view that changes in brain activity are associated with behavioral performance improvements, even when subjects are not conscious of them. To use the decoded fMRI technique, it would be necessary to determine which brain region relates to perceptual learning and how it is activated to achieve perceptual learning for a specific target. Therefore, perceptual learning using the decoded fMRI technique can only be achieved when the participants are able to perceive the target. In contrast, the method using MMN used here can affect these neural changes without identifying the specific brain activity pattern or the regions impacted by individual sound features. This is because the MMN has been widely used and is known as an index of sound discrimination accuracy, and is elicited by any discriminable auditory change, in the absence of a conscious realization of the contrast. In addition, it can be detected without knowing the brain regions or specific brain patterns associated with low-level processes. Therefore, our method enables participants to perceive auditory differences that they could not previously perceive. Compared with expensive fMRI devices, an EEG device is more affordable and accessible, and the MMN response is easy to record. Finally, EEG devices can easily be equipped with various advanced functions, such as stable active electrodes, fast fit caps, and compact mobile setups.

Previous studies have shown that the MMN response is correlated with discrimination accuracy and persistence of sensory memory for sounds. In our study the improvements in discrimination accuracy were confirmed by BAD tests; therefore, it is reasonable to conclude that our neurofeedback method improved discrimination accuracy. Several studies have shown greater amplitude, shorter
related with the degree of impairment in phonological skills, as deficits of pitch discrimination ability and MMN are positively correlated.

**Methods**

**Experimental details.** Throughout each training session, the participants were seated in an antistatic chair in front of a 23-inch computer screen. Stimuli were presented binaurally via earphones. Event-related potential (ERP) responses were measured with the MP150 Data Acquisition System (BIOPAC Systems, Inc. Goleta, California, USA). Responses were recorded with a sampling rate of 500 Hz. A band pass filter of 0.1-35 Hz was applied. Voltage variations caused by horizontal or vertical eye movements were monitored with an electrode attached to the outer canthus of the left eye. Recordings that contained voltage variations due to eye movements or other extracerebral artifacts exceeding ±40 μV were omitted.

**Behavioral auditory discrimination (BAD) test.** In the BAD test, a two-alternative forced choice task was performed, in which the accuracy of behavioral auditory discrimination was assessed using simple sinusoidal tones of 1000 Hz and 1008 Hz. In each trial, two pure tones were presented as a stimulus set with a duration of 100 ms, including 5 ms rise and fall times, in one of four combinations (1000 Hz and 1008 Hz; 1000 Hz and 1008 Hz; 1008 Hz and 1000 Hz; and 1008 Hz and 1008 Hz) (Fig. 1b). The intensity of the stimuli was 85 dB. The stimulus onset asynchrony (SOA) was 500 ms. The order of presentation of the combinations was randomly determined and counterbalanced across trials and the number of trials for each combination was controlled to be equal. Throughout the task, participants were asked to fix their eyes on a solid green disc with a 0.8 deg radius in the center of the monitor. After each trial, a 2 s interval was inserted, consisting of 1 s of white noise as sound interference and 1 s of silence (Fig. 1c). During these intervals, the participants reported whether the two pure tones presented in a trial were different by pressing one of two buttons on a keyboard. A brief break period was provided after each run of 60 trials. The participants performed 300 trials on each day, except on the first day when 600 trials were performed (300 trials before and 300 after the training). Participants whose test accuracy rate exceeded 65% in the pre-training test were excluded and did not participate in any subsequent training or testing.

**Participants.** Sixteen of the 26 participants initially screened with the BAD test (an accuracy rate range of 50–63%) participated in the present study, including 9 men and 7 women. All participants were right-handed, monolingual speakers of Japanese (age, 22–38 years) with normal hearing. Participants were randomly distributed into the neurofeedback group (4 men, 4 women) and control group (5 men, 3 women). The participants gave written informed consent. The study protocol was approved by the local ethics research committee at Osaka University, Japan, and all research was performed in accordance with the ethical standards described in the Declaration of Helsinki.

**Training procedure.** In the learning stage, an auditory stimulus sequence of 1000 Hz and 1008 Hz tones as the standard and deviant stimuli in the oddball paradigm. The intensity and stimulus onset asynchrony (SOA) were the same as the BAD test. The total number of trials was 300 (1000 Hz, 240 trials; 1008 Hz, 60 trials) in each session. The stimuli were presented in a random order. ERPs were recorded with for 300 ms from stimulus onset at Fz (the International 10–20-system for EEG electrode placement). The MMN was calculated from the previous 20 trials (4 deviant stimuli and 16 standard stimuli). First, ERPs for the standard and deviant stimuli were averaged, and then the MMN was obtained by subtracting the average standard ERP from the average deviant ERP. The MMN amplitudes were measured using the frontal (Fz) deviant-minus-standard differences as the peak value with a 100–250 ms interval. Data from the first 20 trials in the learning stage were used to compute the MMN while the size of the solid green disc was fixed. After the first 20 trials, the MMN was updated every 500 ms in parallel with the auditory stimuli. A single session consisted of a sequence of 300 sounds (0.5 s × 300 = 150 s), and 12 sessions were performed on each training day. Each participant
underwent training for 5 days (completed in no more than 10 days), with at least 24 hours between training. The size of the disc (0.4–4.97 deg radius) was updated in response to the MMN amplitude every 500 ms.

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Author contributions
M.C., H.I., H.A. and T.M. designed the experiments. M.C. collected and analyzed the data. H.I. assisted with the experimental setup. M.C., H.I. and Y.N. primarily wrote the manuscript. All authors discussed the results and commented on the manuscript.

Additional information
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