Real-time surgical instrument detection in robot-assisted surgery using a convolutional neural network cascade

Zijian Zhao¹, Tongbiao Cai¹, Faliang Chang¹, Xiaolin Cheng²

¹School of Control Science and Engineering, Jinan, Shandong, People’s Republic of China
²Laboratory of Laparoscopic Technique and Engineering, Qilu Hospital of Shandong University, Jinan, Shandong, People’s Republic of China

E-mail: zhaozijian@sdu.edu.cn

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Surgical instrument detection in robot-assisted surgery videos is an important vision component for these systems. Most of the current deep learning methods focus on single-tool detection and suffer from low detection speed. To address this, the authors propose a novel frame-by-frame detection method using a cascading convolutional neural network (CNN) which consists of two different CNNs for real-time multi-tool detection. An hourglass network and a modified visual geometry group (VGG) network are applied to jointly predict the localisation. The former CNN outputs detection heatmaps representing the location of tool tip areas, and the latter performs bounding-box regression for tool tip areas on these heatmaps stacked with input RGB image frames. The authors’ method is tested on the publicly available EndoVis Challenge dataset and the ATLAS Dione dataset. The experimental results show that their method achieves better performance than mainstream detection methods in terms of detection accuracy and speed.

1. Introduction: Robot-assisted minimally invasive surgery (RMIS) systems, like the daVinci surgical system (dVSS), have gained more and more attention in recent years. Rather than cutting patients open, RMIS allows surgeons to operate by tele-manipulation of dexterous robotic tools through small incisions, which results in less pain and fast recovery time. With RMIS systems, surgeons sit at a console near the operating table and utilise joysticks to perform complex procedures. Such systems will translate surgeons’ hand movements into small movements of the surgical instruments in real time. The location of surgical instruments is a common requirement to provide surgeons with important information for observing tool trajectory and can lighten their burden of finding the instruments during an operation. On the other hand, having real-time knowledge of the motions of the surgical tools can help in the modelling of gestures and skills for the real-time automated surgical video analysis [1], which is good for training the novice surgeons [2]. Hence, in this study, we focus on real-time instrument detection.

Many methods for tool detection have been proposed in the last decade, including optical tracking [3], kinematic template matching [4], image-based detection methods [5], and so on. Nowadays, the image-based (vision-based) methods have become increasingly popular as they require no modification to surgical tool design for providing localisation information [6]. Some early image-based methods utilised low-level feature representations computed over video frames for tool detection, and are comparatively fast. For example, colour segmentation methods [7] by CIELab colour space transformation and thresholding were proposed to extract tool shapes from image frames. Another example of feature representation is gradient features [8] which are often leveraged to retrieve tool edge lines via the Hough transform. However, these methods have significant shortcomings. Noise in image frames, such as lighting change, can easily lead to bad detection results. To overcome these challenges, more robust feature representations, such as scale invariant feature transformation (SIFT) [9] and colour-SIFT [10], have been utilised to detect instruments. Recently, convolutional neural network (CNN)-based methods have become a popular choice for different visual detection tasks such as pedestrian detection, human pose estimation etc. These have also been applied for the analysis of surgical videos, such as instrument presence detection [11, 12], phase recognition [13, 14], tool location [15–17], and tool pose estimation [2, 18]. For example, a cascading model, which consists of a rough location network and a fine-grained search network, was proposed by Mishra et al. [19] to locate the tool tip. In the work of Chen et al. [20], a CNN is trained with the datasets labelled by a line segment detector to detect a tool’s tip, and then the spatial and temporal context algorithm [21] is utilised to detect the tool in real time. These methods exhibit good performance in single surgical tool detection, but they fail to satisfy the need of multi-tool detection. To overcome this problem, a multi-modal CNN based on a faster region convolutional neural network (RCNN) [22] is used by Sarikaya et al. [23] for multi-instrument detection. This method achieves good results for detection accuracy but cannot detect the surgical tools in real time (operating at ~20 fps).

In this Letter, we propose a novel frame-by-frame real-time detection and location method for multi-instruments, which consists of an hourglass network [24] and a modified VGG-16 [25] network. The former heatmap network is used as a fully convolutional regression network to output the heatmaps which represent the location of the instruments’ tip area. The latter performs bounding-box regression on these heatmaps stacked with input RGB image frames. In this way, we can simultaneously predict the tools’ location and perform recognition. Our method is more like human behaviour. Humans glance at an image and instantly know what objects are in the image and their approximate location (heatmap network), and then locate them precisely in the image (bounding-box network). To evaluate the performance of the proposed method, we evaluated our method on the publicly available multi-instrument ATLAS Dione [23] and EndoVis Challenge [2] datasets. Our approach obtains better performance than three state-of-art detection methods in terms of detection accuracy and speed.

2. Methodology

2.1. Heatmap network: The overall design of our CNN-based surgical instrument detection model is shown in Fig. 1. This section will describe the architecture of each sub-network of our detection-regression framework in more detail. In the proposed framework, the heatmap-regression network (Section 2.1) takes the RGB image frame as input and outputs heatmaps which are
confidence maps of the tool tip areas. These heatmaps guide the bounding-box regression network (Section 2.2) to focus on the location of instruments in the input image. Finally, it outputs four real-valued numbers for each tool which encodes the bounding-box position in the image coordinate system.

In our first sub-network, an hourglass network, which takes an RGB image frame of size $640 \times 480 \times 3$ as input, is employed to output $M$ heatmaps which are confidence maps, one for each surgical instrument. As shown in Fig. 1, the network is composed of 5 maximum pooling layers, 4 upsample layers, and 13 convolutional blocks of which each consists of several residual modules [24]. Thus, the output heatmaps have a resolution of $320 \times 240$ pixels. The batch normalisation (BN) layer is added before every rectified linear unit (ReLU) to improve the performance of the network.

We approach a rough instrument location as a binary-classification problem in each heatmap. The ground truth for our regression network is encoded as a set of $M$ binary maps, one for each surgical instrument. As shown in Fig. 2, in each ground-truth heatmap, we set the values within a certain radius around the centre of an object bounding box to 1 as the foreground, and the remaining values are set to 0 as the background. The bigger the object bounding box is, the larger the radius is in the ground-truth heatmap. As we treat the heatmap regression as a multiple binary-classification problem, we train the hourglass network using a pixel-wise sigmoid cross-entropy loss function which is defined as follows:

$$l_h = \frac{1}{M} \sum_{m=1}^{M} \sum_{X(i,j) \in S} \left[ p_{ij}^m \cdot \log \hat{p}_{ij}^m + (1 - p_{ij}^m) \cdot \log (1 - \hat{p}_{ij}^m) \right]$$

where $p_{ij}^m$ and $\hat{p}_{ij}^m$ represent the ground-truth value and corresponding sigmoid output at a pixel location $X(i,j)$ in the $m$th heatmap of size $S$.

2.2. Bounding-box network: For the bounding-box regression network, we apply a modified and extended VGG-16 network originally used for image classification, which contains six convolutional blocks, six pooling layers and three fully connected layers as shown in Fig. 1. The BN layer is added before every ReLU layer. This network takes the heatmaps stacked with the RGB image frame, which is resized to $320 \times 240 \times 3$, as input.
and outputs four real-valued numbers that encode the bounding-box position for each instrument in the image coordinate system. The benefit of this stacked architecture is to guide the bounding-box regression network to focus on the instrument tip area.

The goal of this regression network is to predict a precise region box for each instrument. In contrast to bounding-box regression from the faster RCNN, we train our network using a multiple $L_1$ loss function defined as follows:

$$I_b = \frac{1}{M} \sum_{m=1}^{M} |T_m - \hat{T}_m|.$$  

(2)

where $T_m(t_x, t_y, w, h)$ and $\hat{T}_m(\hat{t}_x, \hat{t}_y, \hat{w}, \hat{h})$ represent the corresponding predicted object bounding box and ground-truth bounding box, respectively, in the image coordinate system, and $T(t_x', t_y', w', h')$ is defined as

$$t_x' = x/W, \quad t_y' = y/H, \quad t_w' = w/W, \quad t_h' = h/H.$$  

(3)

where $x, y, w, h$ denote the centre coordinates of the box and its width and height. The size of the input image frame is $W \times H \times 3$.

3. Experiments and results: To evaluate the performance of the proposed method, we apply the method to two multi-instrument datasets, namely the ATLAS Dione dataset and the EndoVis Challenge dataset. We compare the method with three other mainstream detection methods in terms of detection accuracy and speed.

3.1. Datasets and implementation details: The ATLAS Dione dataset [11] consists of 99 action video clips of 10 surgeons from the Roswell Park Cancer Institute (RPCI) (Buffalo, NY) performing 6 different surgical tasks (subject study) on the dVSS with annotations of robotic tools per frame. Each frame has a resolution of $854 \times 480$. To train our model, we divide the entire set of video clips into two subparts: 90 video clips (20,491 frames) for training and the remaining 9 video clips (1976 frames) for testing. In the MICCAI’15 EndoVis Challenge dataset, there are 1083 frames of $720 \times 576$ pixels from ex-vivo video sequences of interventions. Similarly, this dataset is separated into a training set (876 frames) and a test set (207 frames). The ATLAS Dione dataset is more challenging than the EndoVis dataset because there are more disturbing factors, such as motion blurring, fast movement, and background change.

Before training the proposed framework, we initialise both the hourglass network and the modified VGG-16 network using the default initialisation approach in Pytorch 0.4.1. The image frames fed into our model are all resized to $640 \times 480$ pixels. We apply a two-step training approach: firstly, we train the hourglass network using stochastic gradient descent (SGD) with a learning rate of $5 \times 10^{-3}$, momentum of 0.9, and weight decay of $5 \times 10^{-5}$. Then, we keep this fixed and train the modified VGG-16 network using SGD with initial learning rate of $2 \times 10^{-3}$, momentum of 0.9, and weight decay of $5 \times 10^{-5}$. The learning rate progressively decreases every five epochs by 10%. We implement the proposed detection method and the compared methods (Section 3.2) on Pytorch 0.4.1, Ubuntu 16.04 LTS using an NVIDIA GeForce GTX TITAN X GPU accelerator.

3.2. Comparison with different methods: We compared our method with three other detection methods on the two datasets introduced above. Fig. 3 shows some detection examples in the video frames. In recent years, many object detection models have been applied to surgical instrument detection tasks [1, 23] and achieved great performance. The three anchor-based methods we chose are: Faster R-CNN proposed by Ren et al. [22] (the backbone of VGG-16), Yolov3-416 proposed by Redmon et al. [26] (the backbone of Darknet-53), and Retinanet proposed by He et al. [27] (the backbone of Resnet-50). Non-maximum suppression (NMS) with a threshold of 0.5 is applied to get the final proposals in these methods. Since our proposed anchor-free method does not need extra NMS time, our method has better time efficiency than the other networks. To evaluate the accuracy of our detection method, we use the following evaluation method: if the intersection over union of the predicted bounding box and the ground truth is bigger than 0.5, we consider the instruments to be successfully detected in this frame. As shown in Table 1, our method achieves a mean Average Precision (mAP) of 91.60% for the ATLAS Dione dataset, a mAP of 100% for the Endovis Challenge dataset and mean computation time of 0.023 s for instrument detection in each image frame. This demonstrates that the proposed method achieves better performance than the other three methods.

We also evaluate our method based on a distance evaluation approach. If the distance between the centre of the predicted

![Fig. 3 Detection examples for two datasets. The two columns on the left are from the ATLAS Dione dataset and the final columns are from the Endovis dataset. As shown in the example frames: our method is in blue, Faster RCNN in green, Yolov3 in cyan, Retinanet in yellow, and the ground truth is in red](image)
bounding box and the centre of ground-truth bounding-box is less than a threshold in the image coordinates, the surgical instrument is considered to be correctly detected. The experimental results are shown in Fig. 4. Retinanet achieves a better performance than our approach for the ATLAS Dione dataset at the cost of $3 \times$ lower detection speed. Our method shows the best performance for the Endovis Challenge dataset.

Table 1 Detection accuracy and speed of all methods. AP1 and AP2 represent the detection mAP on the ATLAS Dione and EndoVis Challenge datasets, respectively

| Methods          | mAP1, % | mAP2, % | Detection time (per frame), s |
|------------------|---------|---------|------------------------------|
| Faster RCNN (VGG-16) | 90.36   | 100.00  | 0.064                        |
| Yolov3 (Darknet-53)   | 90.92   | 99.07   | 0.034                        |
| Retinanet (Resnet-50) | 89.39   | 100.00  | 0.070                        |
| our method          | 91.60   | 100.00  | 0.023                        |

Fig. 4 Detection accuracy of surgical instrument tips for the two datasets

Fig. 5 RGB input images of which red channel is replaced by the predicted heatmap of each instrument. The two columns on the left are from the ATLAS Dione dataset and the final columns are from the Endovis dataset. The red coloured area represents the tool tip area. As shown in second image of the first rows, Tool_1 is not in this image, so there is no red coloured area, in other words, the values in the heatmap of Tool_1 are close to 0.

Compared with the other three methods, another advantage of the method is that our method can distinguish between surgical instruments with the same appearance in an image frame. The instruments in two datasets are of the same appearance and the compared method takes them as one class, so they cannot differentiate these instruments. As for our method, the output of the heatmap network is heatmaps which are actually confidence maps, one for each surgical instrument. Fig. 5 shows the RGB input images of which red channel is replaced by the predicted heatmap of each instrument. Based on this, our method can track each instrument although they are of the same appearance in an image frame.

4. Conclusion: In this Letter, we presented a novel frame-by-frame detection method for real-time multi-instrument detection and location using a cascading CNN which consists of an hourglass network and a modified VGG-16 network. The hourglass network is applied to detect a heatmap of each instrument, and the modified VGG is responsible for bounding-box regression. To train our model, we use a two-step training strategy: firstly, we train the hourglass network using a pixel-wise sigmoid cross-entropy loss function, and then keep this fixed and train the...
whole framework using a multiple $L_1$ loss function. The proposed detection model is validated on two datasets: the ATLAS Dione dataset and the Endovis Challenge dataset. The experimental results for these two datasets show that our method achieves a better tradeoff between detection accuracy and speed than the other considered state-of-the-art methods. Moreover, our method can distinguish between instruments of the same appearance while other methods cannot. We think that we can further improve the detection accuracy by replacing VGG-16 with a deeper CNN, but this will reduce the speed correspondingly.

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6 References

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