Deep learning for identification of peripheral retinal degeneration using ultra-wide-field fundus images: is it sufficient for clinical translation?

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In recent years, deep learning (DL) systems have emerged as powerful tools for automated analysis of medical images (1,2). In the field of ophthalmology, DL systems have similarly been successfully applied to a large number of ocular diseases using a variety of ocular imaging modalities (3). From standard colour fundus photography, DL systems have been able to accurately detect significant causes of blindness, such as referable or vision-threatening diabetic retinopathy (DR), age-related macular degeneration (AMD) and glaucoma (4-6). Using optical coherence tomography (OCT) scans, DL systems have also been able to accurately classify AMD and a number of other sight-threatening retinal diseases such as choroidal neovascularization, macular edema and central serous chorioretinopathy (7,8). As the technology continues to develop, clinically validated DL systems are likely to be integral to the future delivery of patient care; particularly in the field of teleophthalmology where DL systems are likely to be deployed, either as assistive or fully-automated decision-making triage and diagnostic tools (9).

In this study, Li et al. developed and validated a DL system for the detection of lattice degeneration and retinal breaks using ultra-widefield fundus images. Ann Transl Med 2019;7:618.

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In this study, Li et al. developed and validated a DL system for the detection of lattice degeneration and retinal breaks using ultra-widefield fundus images (UWF images, which provide a 200° panoramic image of the retina with a single image capture (compared to 45° in standard colour fundus photography). UWF imaging is particularly well-suited to use in teleophthalmology, as it has a rapid acquisition time for the area of retina imaged, and allows better detection of peripheral retinal pathology. The clinical deployment of UWF imaging in the field of DR screening has demonstrated lower rates of ungradable images, reduced image evaluation time, and higher rates of pathology detection (10). DL systems have also been applied to UWF images. To date, these algorithms have been shown to be able to detect a number of sight-threatening ocular diseases; including proliferative DR, AMD, central and branch retinal vein occlusions, macular holes and rhegmatogenous retinal detachments (RRDs) (11-16).

In this study, Li et al. developed and validated a DL system for the detection of lattice degeneration and retinal breaks using UWF Optos images (Optos PLC, Dunfermline, Scotland), on a dataset of 5,606 images from two ophthalmic hospitals in China. All the images were manually classified by three experienced retinal specialists based on the presence or absence of lattice degeneration or retinal breaks [termed notable peripheral retinal lesions (NPRDLs) by the authors], with adjudication by a fourth retinal specialist in cases of disagreement. After training and validation, 12 different DL models were tested on an independent test set of 750 images. These 12 models were derived from four different DL algorithms, each using three different methods for image preprocessing.
Analyzing the performance of these 12 different models showed that InceptionResNetV2 consistently outperformed the other algorithms [average area under the receiver operating characteristic curve (AUC) of 0.996], and that the optimal method of image preprocessing involved applying brightness shift, rotation and mirror flipping augmentation to approximately five times the original size. Their best DL model achieved remarkable performance, with an AUC of 0.999, sensitivity of 98.7%, and specificity of 99.1% for the detection of NPRLs. This DL model was also tested against, and outperformed, two general ophthalmologists in classification of UWF images in the test dataset. Furthermore, they examined heatmap visualizations of all 154 true-positive images, and found that 150 (97.4%) of these images showed accurate localization of the NPRLs in question.

To date, prior studies using DL systems for analysis of UWF images have focused mainly on posterior pole pathology (11-16). This is the first study to examine peripheral retinal pathologies, which are conceivably more difficult to detect even on clinical examination, and known to be more prone to image distortion (globe effect and pincushion distortion). It adds lattice degeneration or retinal breaks to the growing list of ocular diseases that can be potentially detected by DL systems, with potential future applications in screening and teleophthalmology platforms. Both lattice degeneration and retinal breaks increase the risk of RRD, a potentially blinding condition with an incidence of 6.3 to 17.9 per 100,000 population (17). Furthermore, RRD is highly associated with myopia—a growing global problem with a prevalence of 27% in 2010, and predicted to rise to 50% in 2050 (18). As such, an automated solution that enables early detection and treatment of risks factors of RRD will be of huge clinical and economic significance. In this study, the DL model developed performed the task of “automated detection of peripheral retinal pathology” with a high degree of accuracy. Additionally, it utilized a strong reference standard, relying on image classification by three experienced retinal specialists, with a fourth retinal specialist for adjudication. From a technical perspective, the number of different algorithms and image preprocessing techniques used in this study are valuable for moving the field of DL-based analysis of UWF images forward. The heatmap visualization analyses presented further lend credence to the strong performance of the DL system they developed. Heatmap visualizations are often performed in DL-based studies to show a few representative images, and demonstrate qualitatively that the DL system is detecting the actual lesions of interest. However, by taking the extra step to quantify the percentage of all their true-positive cases with accurate heatmap localization (in a similar manner to studies by Kermany et al. and Keel et al.), the authors effectively demonstrate the robustness of their results, and further increase confidence in the performance of their system (19,20). Other studies on DL-based image analysis should strive to adopt a similar methodology for quantifying accurate heatmap visualization, which would help to further address the “black box” phenomenon that is a real barrier to clinical implementation of many DL systems.

This work represents a good “first step” in automating the detection of peripheral retinal features that places an individual at risk for RRD but other challenges lie ahead before clinical deployment of such an algorithm is practicable. Firstly, it is important to remember that this DL system was only tested on the primary dataset. DL systems should be tested on external “testing” datasets, ideally from a variety of different countries, populations and settings, in order to demonstrate that it is truly generalizable to other populations. For example, Bellemo et al. used a DL algorithm for DR screening developed in Singapore, and validated this in population-based DR screening program in Africa (21).

Second, studies on DL systems should endeavor to include more information on the datasets used for development and validation. Besides basic demographic data like age and sex, other relevant information in this context would include refractive status, lens status, and whether or not these patients were symptomatic for floaters or photopsia. Providing detailed information on the datasets used is crucial for clinicians and readers to determine if the DL system developed is likely to be applicable to their own patients.

Third, assessment of image quality is another important factor to consider in the translation of DL systems to clinical practice. In this study, as with many others, poor quality images were screened out manually by human graders—a poignant health economic consideration for clinical deployment. This DL system was also therefore only exposed to and tested on images of good quality. If it were to be clinically deployed, there would have to be an accompanying method of grading or screening images for quality. Human grading of quality before DL system analysis would be time-consuming and resource intensive, and reduce the efficiency of the system. While use of UWF images may reduce the number of ungradable images
compared to standard fundus photography, there is still likely to be a substantial number of these poor-quality images; 10.7% of the UWF images initially screened for this study were deemed to be of poor quality and excluded. Image quality is of particular concern when attempting to screen for peripheral retinal pathology, as any areas of peripheral retina that are obscured by the eyelids or lash artifacts would likely impact the sensitivity of the system negatively. One possible approach to tackling this problem is to first develop a DL algorithm for automated screening of image quality (22,23). This should be applied to all images as a “first cut”, before any subsequent downstream image analysis. In a real-world screening or tele-ophthalmology platform, such ungradable images would either be re-acquired, or referred on to ophthalmology services, to screen for media opacity, cataracts, or other pathology.

Finally, to really have effective translation of DL systems into clinical practice, studies utilizing DL systems for automated image analysis should be designed with the end in mind. As the authors rightly point out, their study did not classify lattice degeneration and retinal breaks independently, which can make clinical application challenging. In clinical practice, lattice degeneration and retinal breaks are lesions with vastly different implications and risks for development of RRD. Consequently, the urgency of ophthalmic assessment and treatment required for the two are quite different. If these two types of lesions were independently classified and the DL system was trained to independently detect them, this would make the system much more effective in clinical practice. Also, while it is important to acknowledge that the DL system may be technically very accurate, and capable of outperforming general ophthalmologists in terms of UWF image classification, the real question in clinical translation is whether it is truly comparable to the “gold standard” evaluation.

DL-based analysis of UWF images has potential to play an important role in the future delivery of teleophthalmology screening platforms. Li et al have developed a novel DL system that is able to detect peripheral retinal pathology such as lattice degeneration and retinal breaks on UWF images, with performance surpassing that of human readers on UWF images. This adds to the growing list of ocular diseases that can potentially be detected from UWF images using DL systems. Not only is significant work required to translate this to meaningful clinical application, but the medicolegal territories of algorithms “missing retinal breaks” remains unchartered. Future work in this area should focus on tackling these real-world challenges, and should be designed with the end goal of scalable and economically viable clinical translation in mind.

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