Quantitative Evaluation of Myocardial Ischemia with Dynamic Perfusion CT

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Abstract
Cardiac computed tomography (CT) could provide the comprehensive morphologic and functional information of coronary artery disease. Coronary CT angiography has been well established for identification and management of symptomatic patients with or suspected coronary artery disease. However, we should know the anatomical stenosis is not the same as the functional one needed to be treated. Dynamic perfusion imaging could lead a non-invasive quantitative evaluation of myocardial ischemia with estimation of myocardial blood flow. In this review, we address the characteristics and advantages of cardiac CT, in particular dynamic perfusion CT for quantitative evaluation of myocardial ischemia.

Keywords: Cardiac CT, Coronary artery disease, CT perfusion, Dynamic, Myocardial blood flow
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Cardiac computed tomography (CT) provides the comprehensive morphologic and functional information of coronary artery disease (CAD). Coronary CT angiography (CCTA) has been well established for identification and management of symptomatic patients with or suspected CAD. Additional pharmacological stress myocardial CT perfusion (CTP) imaging can detect ischemia in patients with CAD (1). Dynamic perfusion imaging could lead a non-invasive quantitative detection of myocardial ischemia with estimation of myocardial blood flow (MBF) same as positron emission tomography (PET). Nowadays, CT fractional flow reserve (CTFFR) from CCTA has become available, which could also detect functional stenosis without stress test (2).

In this review, we address the characteristics and advantages of cardiac CT, in particular the dynamic CTP for quantitative evaluation of myocardial ischemia.

Morphological vs. functional assessment
CCTA has the advantage for coronary visualization with higher temporal and spatial resolution comparing to single positron emission tomography (SPECT)/ positron emission tomography (PET) and magnetic resonance imaging (MRI). The diagnostic ability for detection of anatomically significant stenosis has been demonstrated in patients with both acute and stable CAD with very high negative predictive values (3-5). Therefore, CCTA has been accepted as a primary or secondary diagnostic option for the identification in symptomatic CAD patients with an intermediate likelihood (6). However, we should know the anatomical stenosis is not the same as the functional one to be treated by the percutaneous coronary intervention (PCI). The COURAGE (Clinical Outcomes Utilizing Revascularization and Aggressive Drug Evaluation) trial indicated that PCI based the anatomic estimation of coronary stenosis did not reduce the risk of death, myocardial infarction, or other major cardiovascular events of the stable
CAD patients (7). In contrast, the qualitative and quantitative images from PET and SPECT are used for evaluating functional severity of CAD, which is influenced by both epicardial stenosis and microvascular disease (8). PET derived myocardial flow reserve (MFR), which is calculated by MBF at stress / MBF at rest, has been proposed as a functional parameter of the myocardial ischemia and to provide the incremental risk stratification for cardiac events (9, 10). Quantitative MBF derived from CTP in ischemic heart disease encompasses the functional evaluation of CAD. We reported hyperemic MBF evaluated by CTP had sufficient sensitivity, positive predictive value, and negative predictive value to detect obstructive CAD assessed by invasive coronary angiography in both per-patient and per-vessel analyses (11).

Meta-analysis was recently published to determine the diagnostic utility of 6 cardiac functional imaging modalities such as CTFFR, cardiac MRI, PET, CTP, SPECT and dobutamine stress echocardiography using FFR as the reference standard (12). In a per-patient and a per-vessel analysis, cardiac MRI, PET, CTP and CTFFR expressed a similar high accuracy in detecting functional stenosis compared to SPECT. The advantage of CTP combined with CCTA is a comprehensive diagnostic tool for cardiac ischemia with accurate anatomic assessment in one examination (13).

Static vs. dynamic CT perfusion

CTP acquisitions are broadly separated into two categories as dynamic and static scan protocols. The first pass of iodine contrast media can be used for the hemodynamics to the myocardium. Static single-phase CTP imaging is highly dependent on the contrast material bolus timing. A drawback of static CTP is that the peak attenuation may be missed because only one sample of data is acquired (14). It is difficult to determine whether the static CTP image has been obtained at the optimal scan time that allows for a clear distinction between normal and ischemic myocardium. This is because the optimal scan time varies according to several factors, such as the severity of the coronary lesion and cardiac function. Previous studies reported that the optimal scan time for static single-phase CTP was 2-10s from the time of maximal enhancement in the ascending aorta (15, 16). Evaluation of the ischemic lesion is sometimes difficult only with qualitative evaluation from static scan due to the lower contrast resolution of CT compared to that of CMR. On the other hand, dynamic CTP scan has several advantages such as selection of the appropriate timing from the multiple images and the time density curve to quantify the MBF. Higher exposure dose compared to the static scan and to require the latest multi-detector row CT devices are the disadvantages for the dynamic CTP scan.

Stress first vs. rest first protocol

When the stress imaging is performed first, the detection of myocardial ischemia is optimized because the myocardium is not contaminated by previous injection of contrast material, which may mask an area of ischemia (12). In addition, the administration of beta-blockers and nitrates before the rest image acquisition is allowed without interfering with stress perfusion assessment. On the other hand, rest CCTA first acquisition protocol, followed by a stress acquisition, is more suitable for patients with a low-to intermediate pretest probability of CAD, which allows discontinuation of the protocol when absent or minimal CAD is detected (17).

Quantification of MBF and MFR

The detailed method of dynamic perfusion CT in our institute has been previously reported (11). Dynamic CTP protocol used in our institution is shown in Fig. 1. A non-contrast image is obtained to determine the Agatston score. Then, during a continuous 6-min infusion of adenosine triphosphate (ATP), hyperemic dynamic CTP scan is performed for 25 sec with 50 mL of iodinated contrast (350
mg I/mL) and 30 mL saline chaser (5.0 mL/sec). Resting CTP with a boost scan for CCTA is performed after approximately 15-min interval after the ATP infusion. An intravenous administration of propranolol (up to 10 mg) is used when the heart rate for CCTA is greater than 65 beats per minutes. Both stress and rest images are scanned under the continuous electrocardiogram (ECG) monitoring for prospective triggering. Patients are advised to avoid caffeine (coffee, tea, chocolate, energy drinks, etc) for 24 hours before undergoing stress imaging because it may affect the vasodilator capacity of adenosine during stress (14).

For evaluation of MBF, time attenuation curves are generated from the region of interests of the myocardium and the LV blood cavity. We have developed the algorithm for
calculation of MBF using a single-tissue compartment model with the Renkin-Crone equation validated by $^{15}$O-water PET (13). MFR is calculated as the ratios of hyperemic MBF to resting MBF. Our algorithm is now commercially available (Myocardial Dynamic Perfusion software, Vital workstations, Vital images Inc. USA) with Aquilion ONE VISION edition (Canon medical systems, Japan) (Fig. 2). Per-patient and per-vessel hyperemic MBF and MFR derived dynamic CTP had moderate diagnostic values for detecting obstructive CAD (11). Those parameters can be used to identify the functionally obstructive coronary lesions (18).

Radiation dose reduction

Recently, reconstruction methods have been making remarkable progress which reduce the image noise. Iterative reconstruction (IR) method has been used instead of traditional filtered back projection (19). IR method allows the scan with a lower voltage (80 kV) which leads to the improvement of image contrast and reduction of the amount of contrast medium. We used prospective scan at low tube voltage (80 kV) with the hybrid IR for radiation and noise reduction, and validated the MBF with $^{15}$O-water PET, known as a gold standard for quantification of MBF (11, 15). In these ways, stress and rest myocardial CTP can be done with the lower radiation exposure compared to the combination of traditional SPECT and CCTA scans at 120 kV.

Conclusion

Stress dynamic CTP with CCTA protocol using 80 kV allow comprehensive anatomical and functional assessments regarding quantitative MBF.

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