Experimental artefacts can lead to misattribution of bioactivity from soluble mesenchymal stem cell paracrine factors to extracellular vesicles

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ABSTRACT

It has been demonstrated that some commonly used Extracellular Vesicle (EV) isolation techniques can lead to substantial contamination with non-EV factors. Whilst it has been established that this impacts the identification of biomarkers, the impact on apparent EV bioactivity has not been explored. Extracellular vesicles have been implicated as critical mediators of therapeutic human mesenchymal stem cell (hMSC) paracrine signalling. Isolated hMSC-EVs have been used to treat multiple in vitro and in vivo models of tissue damage. However, the relative contributions of EVs and non-EV factors have not been directly compared. The dependence of hMSC paracrine signalling on EVs was first established by ultrafiltration of hMSC-conditioned medium to deplete EVs, which led to a loss of signalling activity. Here, we show that this method also causes depletion of non-EV factors, and that when this is prevented proangiogenic signalling activity is fully restored in vitro. Subsequently, we used size-exclusion chromatography (SEC) to separate EVs and soluble proteins to directly and quantitatively compare their relative contributions to signalling. Non-EV factors were found to be necessary and sufficient for the stimulation of angiogenesis and wound healing in vitro. EVs in isolation were found to be capable of potentiating signalling only when isolated by a low-purity method, or when used at comparatively high concentrations. These results indicate a potential for containing soluble factors to artefactually increase the apparent bioactivity of EV isolates and could have implications for future studies on the biological roles of EVs.

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Introduction

Many organ systems in adult humans cannot fully regenerate after injury. In many tissues, damaged tissue is replaced with a fibrous scar with little or no functional capacity. This insufficiency underlies some of the most common causes of death and disability in the developed world, including myocardial infarction [1], stroke [2], kidney damage [3] and more. Efforts to develop therapies that allow functional regeneration often make use of multipotent stem cells. In particular, human mesenchymal stem cells (hMSCs) have been used as a source of autologous cells that can be readily obtained from adult patients, overcoming many of the immunological, safety and ethical barriers associated with induced pluripotent stem cells (iPSCs) and embryonic stem cells (ESCs). It was initially thought that after administration to the site of injury, hMSCs would engraft, expand, differentiate, and eventually replace the damaged tissue. Preclinical models in which hMSCs were injected into infarcted hearts and damaged kidneys have shown encouraging results, with some treatments advancing to clinical trials [4,5]. However, it soon became apparent that the observed beneficial effects could not be attributed to expansion and differentiation of the injected hMSCs. In a rat model of myocardial infarction, limitation of infarct size and improvements in heart function were observed within 72 h of administration, too soon to be due to the development of new tissue [6]. HMSCs were found to engraft at low frequency in both hearts and kidneys, with little long-term persistence in tissue [7,8]. It is now generally thought that any benefits from hMSC transplantation are due to paracrine signalling from hMSCs to tissue near or at the site of injury [9,10]. In 2005, it was demonstrated for the first time that hMSC-conditioned culture medium could recapitulate the cardio-protective effects of hMSC transplantation in...
infarcted hearts [11]. Since then, considerable work has been undertaken to establish the key paracrine factors underlying this signalling [6,12–14], as they could have potential as cell-free therapies for a variety of conditions and injuries.

Paracrine signalling from hMSCs has been proposed to act by several mechanisms. In the case of myocardial infarction, multiple studies have found that hMSCs upregulate several key soluble growth factors in response to hypoxia, including vascular endothelial growth factor (VEGF), Insulin-like growth factor 1 (IGF-1), basic fibroblast growth factor (bFGF), hepatocyte growth factor (HGF), Thymosin β4 (Tβ4), and stromal cell-derived factor (SDF1) [6,12–14]. These factors appear to function by reducing apoptosis and encouraging neoangiogenesis within the host tissue. In many cases, these factors have been investigated as potential therapies to improve cardiac remodelling [15,16]. Reno- and neuro-protective signalling from hMSCs has also been attributed to these and other soluble factors [17–23]. These factors have been identified by consensus from multiple studies. In addition, there is also evidence that this paracrine signalling occurs via extracellular vesicles. Extracellular vesicles (EVs) are nanoscale cell-derived lipid vesicles [24]. They are subcategorised by their cellular origin; microvesicles are formed by budding from the plasma membrane, whereas exosomes are released when internal multivesicular bodies fuse with the plasma membrane, releasing their internal vesicles. Although exosomes tend to be smaller than microvesicles and their typical protein populations are not identical, there is substantial overlap in their physical and biochemical properties and as such they are thought to be co-isolated by most if not all isolation methods. Both are known to contain cytosolic and membrane proteins, mRNA, and miRNA, and can transfer these biomolecules to recipient cells either by direct fusion with the plasma membrane or through endocytosis. EV membrane proteins may also interact with cells via ligand/receptor interactions, without uptake or fusion. By these mechanisms, EVs can act as signalling factors [25].

The first indication that EVs might have a role in the paracrine effect was the observation that hMSC-conditioned medium passed through an ultrafiltration membrane to exclude EVs was no longer capable of reducing infarct size in a porcine model of myocardial infarction [26]. These results also implied little or no contribution by soluble factors. Subsequently, EVs were purified and found to be capable of mediating a reduction in infarct size [27]. Since then, EVs from hMSCs have been explored for the treatment of a wide variety of conditions [28–39]. However, few subsequent studies have explicitly re-demonstrated that depleting EVs from hMSC-conditioned medium removes the therapeutic effect; rather, the majority of studies have focused on the use of EVs after their isolation from conditioned medium. There have been recent concerns over the reproducibility of the reported effects of hMSC-EVs, difficulties in establishing a consensus on their mechanism of action, and the quality of characterisation of hMSC-EV preparations [40]. Within the wider EV field, there is an increasing awareness that many of the techniques commonly used for EV isolation are prone to substantial contamination with soluble factors [41–46]. This has so far mostly been discussed in the context of the use of EVs as diagnostic biomarkers [46], and the implications of these observations for the apparent therapeutic capacity of EVs have not yet been explored.

Here, we show for the first time that these and other methodological issues can lead to misidentification of EVs as critical factors in hMSC-mediated signalling. Ultrafiltration of hMSC-conditioned medium removed EVs and reduced proangiogenic signalling, but unexpectedly also removed soluble factors below the membrane pore size. Preventing depletion of soluble factors while maintaining exclusion of EVs fully restored proangiogenic activity in vitro. Chromatographical separation of EVs and soluble protein revealed that proangiogenic and pro-wound healing activity was exclusively associated with soluble protein and not EVs. EVs isolated by a commercial polymer precipitation method stimulated both angiogenesis and wound healing; however, this isolation method was found to co-isolate biologically active contaminants to which this activity could be attributed. More effectively purified EV samples were able to weakly stimulate angiogenesis, but only at concentrations far higher than those at which they were present in conditioned medium, consistent with a minimal role in hMSC paracrine signalling, at least in vitro.

Materials and methods

Cell culture

NIH-3T3, MDA-MB-231 and A549 cells were obtained from the ATCC (Manassas, VA, USA). NIH-3T3 cells were cultured in 4.5 g/L high glucose DMEM with 10% (v/v) FBS and antibiotic/antimycotic (A/A) (Gibco 15240062). MDA-MB-231 and A549 cells were maintained in 4.5 g/L DMEM, supplemented with 10% FBS, 1x non-essential amino acids, 25 mM HEPES and 1x penicillin/streptomycin. Pooled HUVECs (Gibco C0155C) were cultured in M200 media (Gibco M200500) with A/A and
Low-Serum Growth Supplement (LSGS) (Gibco S00310). Human Mesenchymal Stem Cells were obtained from Lonza (Basel, Switzerland). Donor 1 was used throughout the paper; donors 2 and 3 were used to confirm the results from analytical SEC. Donor lot numbers, age, sex, and ethnicity are shown in Table 1. hMSCs were cultured in DMEM with 1 g/L glucose with A/A and 20% (v/v) hMSC-qualified FBS. All cells were grown in Corning (NY, U.S.A) cell culture flasks at 37°C, 5% CO₂. All cell lines were tested and found to be free of mycoplasma.

**Conditioned medium production**

To prepare hMSC-conditioned medium, hMSCs were expanded from p4 stocks to p6, splitting from 1x T175 to 8x T225, and then to 72x T225 flasks. Near-confluent cells were washed once with sterile PBS before addition of 35 mL per flask DMEM (1 g/L glucose) with A/A, without FBS, for 40 h prior to harvest. 2.5 L of conditioned medium was harvested, and each 500 mL of conditioned medium was passed through a 0.45 µm bottle-top filter (Jet Bio-filtration, Guangzhou, China) and aliquoted prior to immediate storage at −80°C. To obtain conditioned medium from MDA-MB-231 and A549 cells, cells were grown to 80% confluence prior a 72 h incubation in basal DMEM, before 0.45 µm filtration as before.

**Ultrafiltration**

Either 3 kDa or 100 kDa Amicon Ultra-15 centrifugal filter devices (Merck Millipore) were used (see text). 12 mL of media was added to the top compartment prior to centrifugation in a fixed-angle rotor at 5000 x g, for 3 min at 4°C. The flowthrough was removed and media topped up to 12 mL. This was repeated, increasing the time of each spin as necessary, until processing was complete.

To block concentrator membranes, 100 kDa centrifugal filter devices were washed once with 18.2 MΩ water by adding 12 mL to the upper compartment prior to centrifugation (5000 x g, 3 min). Subsequently, 12 mL of 1% (w/v) bovine serum albumin (BSA) in PBS was added to the top compartment and left undisturbed for 2 ½ h. The upper compartment was then washed out 4 times with PBS, without centrifugation. The filter was then washed once with PBS by centrifugation before immediate use.

**Size exclusion chromatography**

A 30 × 1 cm Bio-Rad Econo-column was packed to a depth of 28 cm (volume = 22 cm³) with Sepharose CL-2B (Sigma). A flow adaptor (Bio-Rad #7380015) was then fitted. Columns were stored in 20% (v/v) degassed EtOH and washed with > 60 mL particle-free cell culture PBS (Gibco #10010015) prior to use. A valve switching system was used to apply 500 µL of sample before immediately switching to a PBS reservoir. 30 × 1 mL fractions were collected from the point of the switch. Columns were then washed with > 60 mL PBS and 60 mL of 20% EtOH for storage.

**Total exosome isolation**

From 100 mL of pre-processed hMSC-conditioned medium, 750 µL was removed for later analysis, and the remaining media was concentrated to a final volume of 1 mL using 4 × 3 kDa Amicon centrifugal concentrators. From the concentrated media, 165 µL was removed for later analysis. 417 µL of TEI reagent was added to the remaining 835 µL of concentrated medium in a 1.5 mL Eppendorf tube before vortexing to mix. The TEI/concentrated media mix was incubated for 16 h at 4°C before centrifugation (10 min, 10,000 g, 4°C) to pellet precipitated material. Supernatant was thoroughly aspirated, and the pellet was resuspended in 100 µL particle-free PBS by thorough pipetting before immediate aliquoting and storage at −80°C.

**Nanoparticle tracking analysis**

Particle concentration was quantified using a Nanosight NS300 (532 nm laser, SCMOS camera) (Malvern Instruments, Salisbury, UK). EVs were diluted in particle-free water from a Select Fusion Milli-Q water purifier (Suez Water UK, Thame, U.K.) at the point of measurement to a concentration between 10⁸–10⁹ particles/mL. Using NTA V3.0 software, three 60-s videos were recorded and analysed per sample, with software parameters Camera Level 15 and Detection Threshold 5 used, and FTLA smoothing disabled.

**Dot blots**

A 0.45 µm nitrocellulose membrane (Bio-Rad 162–0117) was soaked in Tris-buffered Saline (TBS, Bio-Rad 170–6435) for 10 min, before assembly into the Bio-Dot cassette (Bio-Rad 170–6545). Wells were filled with TBS
and drained under vacuum prior to addition of sample to each well. 100 µL of conditioned medium or 50 µL of SEC fraction samples was added per well and allowed to drain without vacuum. Wells were then washed 3x with TBS, with vacuum, prior to retrieving the membrane and blotting with 5% (w/v) skim milk (Bio-Rad 170–6404) in TBS-T on a rocking platform (1 h., r.t.). The membrane was washed 3x in TBS-T (5 min each) prior to addition of primary antibodies and overnight incubation. Primaries were used at 1:1000 dilution in 5% (w/v) BSA in TBS-T (CD63: 10628D, CD81: 10630D, CD9: 10626D, Thermo Fisher). The membrane was washed as before prior to addition of secondary antibody (1:10,000 in 5% (w/v) BSA/TBS-T, goat anti-mouse 800 nm, Li-COR 926–32210) and incubated in the dark for 1 h. After washing as before, membranes were imaged on a Li-COR Odyssey infrared fluorescence imager. Dot intensity quantification was performed using Image Studio software, generating a relative intensity (R.I) value for each dot that was then normalised to the average value within each experimental replicate (N.R.I).

**Western blots**

Protein was isolated from both cell (crude lysate) and EV (peak fraction) samples. Lysates were prepared in RIPA buffer (Cell Signaling Technology, Danvers, MA, USA) supplemented with phosphatase and protease inhibitors (Roche, Basel, Switzerland), and sonicated on ice for 20 seconds at 20% amplitude using a VibraCell VCX500 sonicator (Sonics & Materials Inc., Newtown, CT, USA). Lysates were gently mixed for 1 h at 4°C, after which they were centrifuged for 10 min at 20,000 x g at 4°C. Supernatants were transferred to clean tubes and pellets discarded. Protein concentrations were determined using the BCA assay (Pierce, Thermo Fisher Scientific, Inc.). 15 µg of protein, mixed with Laemmli sample buffer (Bio-Rad Laboratories, Inc., Hercules, CA, USA) without reducing agent, was loaded unto Mini-protean TGX precast 4–20% gradient gels (Bio-Rad) and separated by SDS-PAGE. Next, protein was blotted onto PVDF membranes (EMD Millipore) prior to antibody incubation and fluorescent imaging as performed with dot blots.

**Cryo-TEM**

SEC-EV peak fractions were pooled and concentrated as previously described. TEI-EV samples were used without further concentration. Holey Carbon 200 mesh Grids (Electron Microscopy Supplies) were glow-discharged (15 sec O₂/H₂ 1:1) with a Solaris plasma cleaner (Gatan, Pleasanton, CA, U.S.). Samples were prepared with a Leica EM GP plunge-freezer. Sample grids were prepared by adding 4 µL of sample within an environmental chamber (20°C, 90% relative humidity). Excess sample was blotted away on filter paper prior to plunging into liquid ethane. Samples were stored and transferred in liquid nitrogen in a Gatan model 914 cryo transfer holder. Samples were imaged at −170°C in a JEOL 2100 Plus Transmission Electron Microscope (JEOL, Tokyo, Japan) at 200 kV, using a Minimum Dose System software. Images were acquired with an Orius SC 100 camera (Gatan) at 30 k magnification over 5-sec exposure time.

**ELISA**

The VEGF Human ELISA kit (Thermo Fisher K0H012) was used according to manufacturer instructions.

**Nano-orange**

The NanoOrange assay kit (Thermo Fisher N6666) was used according to manufacturer instructions.

**Tubule formation assay**

HUVECs were thawed from p2 stocks and grown for 6 days prior to the assay. 6 h prior to use, HUVECs were transferred to basal M200 media. 1 h prior to use, GFR Geltrex (Gibco A1413202) was mixed at a 6:1 ratio with ice-cold PBS, before addition (on ice) of 10 µL of diluted Geltrex to each well of an Ibidi 96-well angiogenesis plate (Ibidi, 89646). The plate was spun in a plate centrifuge at 50 g, 60 s, before incubation at 37°C for gelation. HUVECs were detached with Trypsin, centrifuged and resuspended in basal M200 medium before measurement of viable cell concentration with a Countess II FL cell counter (ThermoFisher). Viable cell concentration was adjusted to 10⁵/mL. Cells, samples and buffers (DMEM or PBS) were combined and added gently to wells. Sample volumes are shown in Table 2.

After 16 h incubation at 37°C, 5% CO₂, 20 mL of 2 µM CaLein-AM (Invitrogen C3099) in basal M200 media was gently added to the top compartment of the plate before returning to the incubator, protected from light, for 20 min. The plate was then washed once and imaged using an Axio Observer live cell imaging microscope with an HXP 120 light source (Zeiss) at 37°C, 5% CO₂. A 2.5X objective was used and the entirety of each well was imaged.

Images were imported, cropped circularly to remove well edges, and converted to a binary image using a manually set threshold using FIJI [47]. The threshold was set to highlight all tubule structures without
including background. The binary images were then analysed using the “Angiogenesis Analyzer” plugin [48]. Total tubule length was used to compare the pro-angiogenic activity of samples.

**Transfection**

Cytolight Green Lentivirus (Incucyte 4481, Sartorius, Göttingen, Germany) was used according to the manufacturer’s instructions to generate a GFP-positive NIH-3T3 cell line (GFP-3T3).

**Scratch assay**

24-well plates were coated with Collagen-I (100 μL/well, 50 μg/mL, in 0.02 N acetic acid, Corning 354236) for 2 h before aspirating fluid and allowing to dry fully for at least 3 h. Coated plates were stored at 4°C and used within 2 weeks. GFP-3T3 cells were seeded at 50 K cells/well 24 h prior to the assay. After 24 h, a monolayer had formed. A scratch was made across the centre of each well using a p200 pipette tip steadied with a ruler. The media was replaced with fresh basal DMEM, and each scratch visually inspected. Scratches that were ragged, wider than the field of view or less than 1/3rd of the width of the field of view were excluded. The basal DMEM was removed before adding samples and controls, all diluted 1:1 in fresh basal DMEM (C+: DMEM + 10% (v/v) FBS, C-: sample buffer (DMEM or PBS)). Each well was imaged for GFP fluorescence at 3 manually selected positions along the scratch, every hour for 15 h (16 timepoints) using an Axio Observer live cell imaging microscope (Zeiss). Images were analysed with FIJI [47], using the “MRI Wound Healing Tool” [49]. The area of the gap in each image was quantified, and the rate of area reduction until closure determined by linear regression for each individual image set. Image sets with improper gap/cell segmentation (due to reflections, uneven illumination or floating cells) were excluded from the final calculation of each well’s closure rate. Three wells were used for each condition, forming three technical replicates.

**Statistics**

Calculations were performed using Graphpad Prism 8. Experiments were designed such that paired or within-subjects statistical tests could be used. For comparison of two groups with paired replicates, 2-tailed paired Student’s t-tests were used. For comparison of three or more groups with paired replicates, one-way within-subjects ANOVAs (Analysis of Variance) were used, with a post-hoc Tukey’s HSD test (for comparison of all means) or Dunnett’s test (for comparison to a single control value). Numerical data within body of text is expressed as mean ± standard deviation.

**EV-TRACK**

We have submitted all relevant data of our experiments to the EV-TRACK knowledgebase [50] (EV-TRACK ID: EV190075).

**Results**

We initially sought to recapitulate the pioneering observation that passage through an ultrafiltration membrane depletes the bioactivity of hMSC conditioned medium (hMSC-CM) [26,27]. HMSC-conditioned medium was prepared and passed through a 100 kDa Molecular Weight Cut-Off (MWCO) centrifugal spin filter (Figure 1(a)), collecting five sequential ~20 mL samples (Flowthrough 1-5, or FT1-5). It was expected that EVs would be retained while soluble proteins smaller than 100 kDa would pass through unimpeded. To establish the presence and concentration of EVs in the hMSC-conditioned medium and the flowthrough, the particle concentration was quantified by nanoparticle tracking analysis (NTA) (Figure 1(b)) and the availability of CD63 epitopes investigated by dot blotting (Figure 1(c)). Nanoparticles and CD63 were detected in the hMSC-conditioned medium but not in any of the flowthrough fractions, confirming that EVs were present in conditioned medium but reduced to undetectable levels after passage through the spin filter.

We next evaluated the pro-angiogenic activity of the hMSC-conditioned medium and flowthrough samples using an *in vitro* human umbilical vein endothelial cell (HUVEC) tubule formation assay, in which HUVECs were incubated for 16 h on a growth factor-reduced basement membrane mimic in the presence of 1:1 v/v fresh basal medium and sample. Cells were visualised by Calcein-AM fluorescence and the total length of the tubules formed was quantified for each well using FIJI, as described in the methods. We observed that the *in vitro* pro-angiogenic activity of the conditioned medium was

| For 12 replicates | M200 (basal) | M200 + LSGS (10x) | Sample/buffer | Cells at 1 x 10⁵/mL |
|------------------|-------------|------------------|----------------|-------------------|
| Positive Ctrl    | 120 µL      | 60 µL            | 300 µL (buffer)| 120 µL            |
| Negative Ctrl    | 180 µL      | 0 µL             | 300 µL (buffer)| 120 µL            |
| Samples          | 180 µL      | 0 µL             | 300 µL (sample)| 120 µL            |
Figure 1. Contents and signalling properties of hMSC-conditioned medium after 100 kDa ultrafiltration. Media (CM) was passed through a 100 kDa membrane and collected in sequential ~20 mL batches (FT1-5), as described in the main text. (a) Schematic of experimental workflow. CM = Conditioned medium, FT = Flowthrough. (b) NTA measurements of i) concentration and ii) size distribution (of CM samples), N = 3, n = 3 x 60s videos, mean ± SD shown. Particles were only detected in CM (1-way within-subjects ANOVA and post-hoc Dunnett’s test vs DMEM control). (c) Dot blots against CD63. CD63 was only detected in CM. Independently prepared replicate samples were blotted onto the same membrane and analysed simultaneously (N = 3, representative blot shown). (d) Representative whole-well images of tubule structures. Images inverted for clarity. Scale bar = 1 mm. (e) Quantification of total tubule length in tubule formation assay. All samples besides FT1 had a greater proangiogenic activity than DMEM (N = 3, n = 12, mean ± SD of n shown for each N (replicates 1–3, R1-3), 1-way within-subjects ANOVA and post-hoc Dunnett’s test vs DMEM control). (f) ELISA against VEGF. VEGF was reduced relative to the level in CM in FT1 and FT2 only (N = 3, n = 2, mean ± SD shown, 1-way within-subjects ANOVA and post-hoc Dunnett’s test vs CM). *: p < 0.05, **: p < 0.01, ***: p < 0.001, ****: p < 0.0001.

completely removed in the first ~20 mL of flowthrough (Figure 1(d,e)), consistent with results reported elsewhere [26,27]. However, the subsequent fractions exhibited increasing pro-angiogenic activity, which rose to a level similar to that of the unfiltered hMSC-conditioned medium. As we did not detect EVs in these fractions, we hypothesised that non-EV factors might contribute to signalling. Many small protein signalling factors secreted by hMSCs have been implicated in their signalling [6,12–14,17,18]. Of these, we selected VEGF to serve as a representative indicator of the presence and abundance of these factors as a group and evaluated its concentration in the conditioned medium and flowthrough. Sample analysis with an Enzyme-Linked Immunosorbsent Assay (ELISA) found that VEGF was present in the unfiltered conditioned medium, significantly depleted in the first two flowthrough fractions, but progressively increased in subsequent flowthrough fractions to a level similar to that of the unfiltered conditioned medium (Figure 1(f)). This matched the pattern of bioactivity observed in the tubule formation assay, indicating contribution by soluble factors.

VEGF exists in solution as a 45 kDa homodimer [51] and so the observation that it did not pass through a 100 kDa pore size membrane unimpeded was unexpected. We attributed this observation to attractive electrostatic or hydrophobic interactions between the soluble factors and the ultrafiltration membrane. Under this model, the membrane surface becomes passivated as progressively more protein is adsorbed and removed from the flowthrough. Eventually, a passivating layer of protein builds up on the surface, blocking subsequent protein/surface interactions and allowing unimpeded passage of proteins below the membrane pore size. While these effects may not be significant when filtering a large quantity of protein, it could have a significant impact on dilute solutions
containing low-abundance soluble factors such as VEGF. We tested this hypothesis by passing hMSC-conditioned medium through membranes that had been pre-passivated with 1% (w/v) Bovine Serum Albumin (BSA) (Figure 2).

No particles (Figure 2(a)) or CD63 epitopes (Figure 2(b)) were detected in the flowthrough of pre-passivated or untreated membranes. However, the loss of VEGF was substantially mitigated by pre-passivation, with 57.6 ± 2.6% recovery compared to 8.3 ± 0.9% for the un-passivated control (Figure 2(c)). The same pattern was seen in stimulation of in vitro angiogenesis (Figure 2(d,e)). Flowthrough from non-passivated filters had a reduced capacity to stimulate angiogenesis compared to the unfiltered conditioned medium, whereas the flowthrough from pre-passivated filters retained its original pro-angiogenic capacity. Non-conditioned medium passed through the membrane did not stimulate angiogenesis compared to the negative control, with or without membrane pre-blocking. We concluded that in our experimental system the reduction of pro-angiogenic signalling by ultrafiltration was artefactual rather than due to the depletion of a critical factor larger than 100 kDa.

For subsequent experiments, we chose to also investigate the ability of hMSC-conditioned medium-derived material to stimulate fibroblast migration in a scratch-wound model of wound healing. The inclusion of this model allowed us to test whether our observed results were specific to our tubule formation assay. As it was necessary to concentrate hMSC-conditioned medium in order to observe significant stimulation of wound healing, it was also necessary to investigate whether this concentration step could cause a bias in component recovery or a loss of stimulatory activity.

Figure 2. Effects of membrane surface BSA-blocking on 100 kDa ultrafiltration of hMSC-CM. Membranes were either BSA-blocked (-B-FT) or left unblocked (-FT) prior to filtration of 10 mL of CM or DMEM. (a) NTA measurements (3 x 60 s videos/sample, N = 3, mean ± SD shown) of i) particle concentration and ii) size distribution (of CM sample). Particles were only detected in CM (1-way within-subjects ANOVA and post-hoc Dunnett’s test vs DMEM control). (b) Dot blots against CD63. CD63 was only detected in CM. Independently prepared replicate samples were blotted onto the same membrane and analysed simultaneously (N = 3, representative blot shown). (c) ELISA against VEGF. % recovery of VEGF in CM for each sample is shown (N = 3, n = 2, mean ± SD shown). (d) Quantification of total tubule length in tubule formation assay (N = 3, n = 12, mean ± SD of n shown for each N (replicates 1–3, R1-3)). (e) Representative whole-cell images of tubule structures formed in (d). Images inverted for clarity. Scale bar = 1 mm. Samples are significantly different unless they share a letter (p < 0.05, one-way within-subjects ANOVA and post-hoc Tukey’s HSD test).
To investigate this, 100 mL of hMSC-conditioned medium was concentrated against an ultrafiltration spin filter. A 3 kDa MWCO membrane was used in order to retain both EVs and soluble protein (Figure 3). Conditioned medium (1x) was concentrated 5-fold (5x) and 25-fold (25x). The 25x concentrated conditioned medium was then diluted 5-fold (5x-d) and 25-fold (1x-d) with fresh basal DMEM. Any loss due to the concentration process was anticipated to manifest as differences between the unconcentrated and the concentrated/re-diluted samples (i.e. 5x vs 5x-d, 1x vs 1x-d). It was found that concentration led to a significant decrease in the total number of particles (Figure 3(a)) but no significant loss of VEGF (Figure 3(b)). CD63 epitopes were detected in all samples (Figure 3(c)). Importantly, the ability of hMSC-conditioned medium to stimulate tubule formation (Figure 3(d)) and wound healing (Figure 3(e)) was unaffected by concentration/dilution. It therefore appeared that although sample recovery after concentration was biased in favour of non-EV factors, the factors responsible for stimulation were recovered without significant loss. This was consistent with our previous observations that EVs were dispensable for stimulation of our assays.

Our results so far had indicated that EVs were not necessary for stimulation of angiogenesis, and their loss during concentration of conditioned medium did not impact wound healing in vitro. However, the possibility remained that EVs could stimulate angiogenesis and wound healing independently of soluble factors. We used analytical Size Exclusion Chromatography (aSEC) to separate the components of pre-concentrated (3 kDa, 100 mL -> 0.5 mL) hMSC-conditioned medium by size. 30 x 1 mL fractions were collected. The nanoparticle concentration was quantified in F6-25, and the presence of EV marker proteins (CD63, CD81 and CD9) was determined as before by dot blots on each fraction (Figure 4(a)). Antibodies had been previously validated by Western blot (Figure S1). The majority of EVs appeared to elute in a major peak at F9-10, as defined by particle concentration and the intensity of dot blots against EV markers. However, one or more EV markers were detectable up to F20, with an apparent minor secondary peak detected by all markers and NTA at F18. EVs were not detectable beyond F20.

The protein concentration in each fraction was quantified (Figure 4(b)). Protein was observed between F18-F25, with a peak between F21-22, but was not detected in association with the EV peak. However, as the peak EV concentration was measured to be ~2 x10^{10} particles/mL, pure EVs are reported to have a particle to protein ratio of approximately ~3 x10^{16} particles/μg [42] and the limit of detection for the protein quantification assay was ~1 μg/mL, this observation was consistent with the presence of high-purity EVs. An ELISA against VEGF was performed on pooled adjacent fractions (Figure 4(b)). This analysis revealed the presence of VEGF between F19/20 – 25/26, with a peak at F21/22, consistent with the elution profile of soluble proteins. We concluded that our aSEC setup was capable of separating the majority of EVs from the majority of soluble factors, with a small zone of overlap between F18-20.

We subsequently performed our tubule formation and scratch-wound assays on pooled adjacent fractions (excluding F1-2) (Figure 4(c,d)). For both assays, a significant increase in activity was observed only between F17/18 – F25/26, the fractions containing the highest levels of soluble protein and VEGF. Contrarily, there was no detectable stimulation of angiogenesis or wound healing in the fractions containing the highest concentrations of EVs. The aSEC experiments were repeated with two additional independent hMSC donors (Figures S2-3) and similar results were observed, with no EV-associated stimulation and robust soluble protein-associated stimulation. The average modal EV diameter at F9 across all 3 donors was 141 ± 17.3 nm (125 ± 11.3 nm when a single outlier was excluded [Table S1]). As before, the concentrators were found to preferentially recover VEGF, but there was no difference detected between EV and VEGF recovery from aSEC, either overall or in the peak fractions (Figure S4).

Our evidence so far indicated that the majority of pro-angiogenic and pro-migratory signalling from hMSC-conditioned medium was mediated by conventional soluble factors and not by EVs. However, EVs are widely reported to potentiate wound healing and angiogenesis. We hypothesised that this discrepancy could be partially due to differences in EV purity, given that there is increasing concern that many EV purification protocols do not effectively remove contaminants. In order to investigate whether less stringent purification procedures could lead to artefactual results by co-isolation of biologically active soluble factors, we chose to purify EVs using a commercial kit for polymer precipitation-based EV isolation (Total Exosome Isolation Reagent, or TEI). Polymer precipitation remains in common use as a primary isolation method; however, it has been reported that the resulting EV samples may be impure [44]. 100 mL of conditioned medium was concentrated against a 3 kDa membrane to a final volume of 1 mL as before. EVs were isolated from this 100x concentrated medium according to manufacturer instructions, resuspending EVs in 0.1 mL of particle-free PBS.
Figure 3. Effects of concentration on contents and signalling properties of hMSC-CM. CM was concentrated 5x against a 3 kDa membrane, then 25x, before subsequent dilution to 5x (5x-d) and 1x (1x-d) concentrations. (a) NTA concentration measurements of samples, expressed as i) absolute concentration values and ii) % recovered from input CM. (N = 3, n = 3 x 60s videos, mean ± SD shown). (b) ELISA against VEGF, expressed as i) absolute concentration values and ii) % recovered from input CM. (N = 3, n = 2, mean ± SD shown). (c) Anti-CD63 dot blots. Independently prepared replicate samples were blotted onto the same membrane and analysed simultaneously. (d) i) Quantification of total tubule length in tubule formation assay (N = 3, n = 12, mean ± SD of n shown for each N (replicates 1–3, R1-3)). (d) ii) Representative whole-well images of tubule structures formed in i). Images inverted for clarity. Scale bar = 1 mm. (e) i) Quantification of wound closure rate for each condition (N = 3, n = 3, mean ± SD shown for each N (replicates 1–3, R1-3)). (e) ii) Representative images of scratch wounds for each condition are shown for t = 0 h and t = 15 h. Scale bar = 100 μm. Samples are significantly different unless they share a letter (p < 0.05, one-way within-subjects ANOVA and post-hoc Tukey’s HSD test). Where plotted on a logarithmic axis, data were log_{10}-transformed prior to statistical analysis.

EVs isolated by TEI were able to significantly stimulate both angiogenesis (Figure 5(a)) and wound healing (Figure 5(b)) at minimum in-assay concentrations of $2 \times 10^9$ and $5 \times 10^9$ particles/mL respectively. This is in contrast to the lack of any stimulation by higher concentrations of particles from the F9-10 EV peak after analytical SEC (Figure 4, S1, S2). The average combined particle concentrations of F9 and F10 across all 3 donors was $1.11 \times 10^{10}$ particles/mL – consequently, the average in-assay concentration would have been $5.55 \times 10^9$ particles/mL due to dilution. This is a higher concentration than the minimum threshold for stimulation by TEI-isolated EVs for both the tubule formation and wound healing assays. We therefore concluded that there was a difference in the content of these EV isolates besides the number of particles. We assessed the particle (Figure 5(c)) and VEGF concentrations (Figure
5(d)) of the conditioned medium, concentrated conditioned medium, and final TEI-isolated EV samples to determine whether TEI might have co-isolated VEGF or other contaminants. We also confirmed the presence of the EV marker CD63 in all samples by dot blots as before (Figure 5(e)), and the size distribution of the TEI-EVs (modal diameter = 115.8 ± 10.6 nm) (Figure 5(f)). The protein concentration of the TEI-isolated EV sample was 589.2 ± 20.9 μg/mL, an estimated yield of 0.59 μg per mL of the initial conditioned medium. TEI isolation removed 98.7 ± 0.2% (by mass) of VEGF from the concentrated conditioned medium; however, due to the high initial concentration and low final volume, the final concentration of VEGF was over an order of magnitude higher than that of conditioned medium: 2.52 ± 0.67 μg/mL. The particle-to-protein ratio in the final isolate was calculated to be 7.84 ± 0.46 x 10^6 particles/μg. Values below 1.5 x 10^9 are typically considered impure [42]. The ratio of particles-to-VEGF was 1.98 ± 0.79 x 10^6 particles/pg. The average F9 particle concentration across all 3 donors was 1.44 x 10^10 particles/mL, and the F9-10 value was 1.11 x 10^10, as previously mentioned. At these ratios, the
expected associated mean protein concentration at F9 would have been 18.3 μg/mL, and the VEGF concentration at F9-10 would have been 56.1 pg/mL. These values are well within the detection limits of each assay; however, no protein was detected in F9 or VEGF in F9-10 (Figure 4). It was therefore concluded that they were likely present not as EV-associated material but as contaminants that had been removed by SEC but not TEI. This was consistent with Cryo-TEM images that showed that although both SEC-isolated EV samples and TEI-isolated EV samples contained vesicular structures of the expected diameter (Figure S5), TEI-isolated EV samples also contained dark amorphous clusters of material that may have been non-vesicular protein aggregates. These results indicated that the activity of our TEI-isolated EV samples was driven by the presence of contaminating soluble factors and not by EVs.

In previously reported research, the quantity of EVs that were used to stimulate angiogenesis or wound healing has not typically been explicitly compared to the quantity of EVs in the original conditioned medium. Doses used are often given in terms of protein concentrations rather than particle concentrations; this metric is susceptible to influence from non-EV protein contaminants. Additionally, EV-associated protein alone cannot readily be measured in conditioned medium prior to isolation. Hundreds of mL of conditioned media are often required to purify sufficient EVs for downstream use, despite the stimulatory activity originally having been apparent in unconcentrated, unprocessed medium.
We hypothesised that EVs were not a major signalling component at the concentrations at which they were present in our conditioned medium, but that it might be possible to stimulate our assays using SEC-purified EVs if they were used at a much higher concentration. EVs were purified in batches from 1.4 L of hMSC-conditioned medium, concentrating conditioned medium to 1.5 mL with centrifugal ultrafiltration (100 kDa MWCO) prior to separation of 3 × 0.5 mL batches using SEC as in Figure 4. Fractions previously established to contain the major EV peak (F8-14) were pooled and further concentrated by ultrafiltration. To maximise the amount of EV material available for stimulation, only particle and protein concentration measurements were performed on the final samples. The mean particle-to-protein ratio was 5.23 ± 0.31 × 10^8 particles/µg. This indicated moderate but not exceptional purity, suggesting that the increased concentration of the conditioned medium prior to column loading might have slightly affected particle/protein separation. Modal particle diameter was 116 ± 15.8 nm.

It was found that SEC-purified EVs at in-assay concentrations of 2 × 10^10 particles/mL and 1 × 10^11 particles/mL were weakly stimulatory compared to the negative control (Figure 6(a)) in a tubule formation assay. To allow direct comparison to conditioned medium, SEC-purified EVs were transferred to DMEM by ultrafiltration. This sample and 100-fold concentrated conditioned medium were both measured by NTA and diluted to matched particle concentrations. Modal pure EV particle diameter was 110 ± 9.4 nm. No significant stimulation of tubule formation by SEC-purified EVs was observed at any concentration (Figure 6(b)); correspondingly, conditioned medium was stimulatory at all particle concentrations, the lowest of which was 125x lower than the highest SEC-EV concentration.

**Discussion**

In the work presented here, it was found that the presence or absence of EVs did not affect the ability of hMSC-conditioned medium to stimulate *in vitro* models of angiogenesis and wound healing. Rather, smaller soluble factors such as VEGF appeared to be responsible. Ultrafiltration of conditioned medium to deplete EVs, which was previously used to implicate the criticality of EVs to therapeutic hMSC paracrine signalling in *in vivo* models of cardiac ischaemia, was found to generate misleading results due to off-target depletion of soluble factors. HMSC-EVs were only found to stimulate angiogenesis and wound healing *in vitro* when either insufficiently purified away from other factors or when used at concentrations far higher than those at which they were present in conditioned medium. The extent to which these methodological risks may have affected previously-reported hMSC-EV studies is unclear, as many do not report EV-depleted conditioned medium controls, sufficiently detailed data describing EV sample purity, or the EV doses used in relation to the quantity of EVs in the source material.

However, it is important to note that this study does not exclude the possibility that hMSC-EVs are

**Figure 6.** Pro-angiogenic activity of SEC-isolated EVs. (a) Assay with EVs in PBS. (a) i) Quantification of total tubule length. (N = 3, n = 8–10, mean ± SD of individual replicates shown (replicates 1–3, R1-3)). (a) ii) Representative whole-well images of tubule structures formed in Ai. (b) Assay with EVs in DMEM and CCM. (b) i) Quantification of total tubule length. (N = 3, n = 10, mean ± SD of individual replicates shown (replicates 1–3, R1-3)). (b) ii) Representative whole-well images of tubule structures formed in b) i). *: p < 0.05, **: p < 0.01, ***: p < 0.001, ****: p < 0.0001 (one-way within-subjects ANOVA and post-hoc Dunnett’s test against C-). Scale bar = 1 mm.
genuinely capable of stimulating regenerative processes under other experimental conditions in vitro or in vivo. HMSC phenotype is known to be affected by culture condition. Our protocol for EV collection involved the culture of hMSCs in basal DMEM, with no supplementation by EV-depleted FBS or exogenous growth factors. This was necessary in order to allow a direct comparison between hMSC-secreted EVs and soluble factors. EVs isolated from hMSCs cultured in basal medium in normoxic 2D culture (as in this study) have been previously reported to have beneficial effects in multiple models of disease [52–57], including in vitro models of wound healing and angiogenesis similar to those presented here [55–57]. However, it may be the case that some culture conditions produce viable, potent hMSC-EVs in sufficient quantities and that the basal conditions required in this study do not. HMSC-EVs have been widely reported to have various beneficial therapeutic effects and assessing the whole spectrum of culture conditions, cell sources, isolation methods and therapeutic applications is beyond the scope of this study. We suggest that our results indicate a “caution signal” – in effect, a requirement for greater awareness of the potential for contamination by non-EV factors to lead to apparently positive results. The methodological hazards identified in this study are relevant to EV bioactivity research outside of hMSC-EV signalling. To the best of our knowledge, co-depletion of soluble factors when removing EVs from conditioned medium by ultrafiltration has not been previously reported. In our study, this led to artefactual attribution of pro-angiogenic signalling to EVs. Polymer precipitation-based methods for EV isolation remain in common use despite concerns over their ability to remove contaminants. We are not aware of any previous demonstration that co-isolated contaminants are active in signalling, nor that their activity can be misattributed to EVs.

We also identified the quantity of EVs used as a potential methodological point of concern. The quantity of EVs in the final isolate used for functional testing is not typically compared to the quantity of EVs in the initial conditioned medium or biofluid. Additionally, cells simultaneously secrete EVs and soluble factors, but cell-derived soluble factors are normally discarded during the purification process and may not be distinguishable from soluble factors added to support cell growth. This means that the respective contributions to signalling of EVs and soluble factors cannot typically be simultaneously evaluated or compared. Under these circumstances, EVs that are only weakly stimulatory compared to other cell-secreted factors could be used at a far higher concentration than that at which they were originally present and then found to be able to stimulate the effect originally stimulated by conditioned medium. The context of the higher potency of other factors would be absent, leading to an erroneous impression that the EVs under investigation have a more critical role in signalling than may be the case.

Conclusions

We unexpectedly found that extracellular vesicles were dispensable for pro-angiogenic and pro-migratory paracrine signalling from hMSC-conditioned basal media in vitro. Previously undescribed experimental artefacts relating to below-cut-off protein depletion by ultrafiltration membranes, co-isolation of soluble protein by less-stringent purification, and experimental usage of comparatively high EV concentrations were all able to obscure this result and led to apparently positive results incorrectly indicating EV function. HMSC-EVs produced and assessed in a variety of experimental conditions have been widely reported to stimulate angiogenesis and wound healing, and EVs may nevertheless genuinely contribute to signalling under other conditions not evaluated here. We interpret our results to be a “caution signal”, indicating a strong requirement to be aware of these experimental hazards when designing and conducting studies on EV bioactivity, including those unrelated to hMSCs.

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Data access statement

Raw data are available upon request from rdm-enquiries@imperial.ac.uk.

Disclosure statement

No funding agency was involved in the study design, data collection, data management, analysis, interpretation or preparation of the manuscript. No conflicts of interest are declared.
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