Association of Relatively Short Posterior Mitral Leaflet With Mitral Regurgitation in Patients With Atrial Fibrillation

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**Background:** The underlying mechanism of mitral regurgitation (MR) in atrial fibrillation (AF) is an isolated annulus dilation caused by left atrial (LA) remodeling. However, the association of mitral valve (MV) geometry with MR in AF patients remains unclear.

**Methods and Results:** We studied 96 AF patients with preserved left ventricular ejection fraction (LVEF). MV geometry was evaluated with 3-dimensional transesophageal echocardiography (3D-TEE). Mitral annulus area of the MR group (n=11, ≥ moderate) was significantly larger (10.6±1.8 vs. 8.2±1.5 cm², P<0.0001), and relative posterior mitral leaflet (PML) area (PML area / mitral annulus area) was significantly smaller (0.51±0.06 vs. 0.57±0.01, P=0.002) than in the non-MR group (n=85, < moderate). Multivariate logistic regression analysis showed that, in addition to LA volume index (LAVI), a relative PML area was independently associated with MR. For sequential logistic regression models to determine the association of MR, clinical variables including age, gender and LVEF were improved by the addition of LAVI (P<0.001) and was improved by addition of mitral annulus area (P=0.01), and further improved by addition of relative PML area (P<0.001).

**Conclusions:** A relatively short PML plays an important role in the development of MR in AF patients. Assessment of MV geometry by 3D-TEE may thus have clinical implications for better surgical management of AF patients with significant MR.

**Key Words:** Atrial fibrillation; Echocardiography; Mitral regurgitation; Mitral valve

Atrial fibrillation (AF) is the most common arrhythmia and is associated with several important cardiovascular events, including impaired quality of life, embolism events, heart failure (HF), and death.1–6 AF and HF are frequently observed to coexist in clinical practice. AF causes left atrial (LA) remodeling and enlargement, with the latter possibly resulting in mitral annular dilatation, which in turn may cause progressive mitral regurgitation (MR), a potential mechanism by which AF induces HF despite the absence of left ventricular (LV) remodeling. Thus, the underlying mechanism of MR in AF is thought to be isolated annulus dilatation by LA remodeling, known as Carpentier’s functional classification Type I.7 Mitral leaflets are able to adapt by means of some compensatory enlargement in response to mechanical stretching resulting from mitral annular dilatation caused by LA remodeling in AF patients. On the other hand, AF patients with significant MR are often seen in clinical practice to have a posterior mitral leaflet (PML) that is shortened in comparison with the anterior mitral leaflet (AML) (Figure 1).

It has been recently reported that the development of MR in AF patients is associated with not only mitral annular dilatation caused by LA enlargement, but also with a multiplicity of other factors.8–12 However, the association of mitral valve (MV) geometry, especially in terms of the shortened PML, with MR in AF patients remains unclear. The purpose of our study was, therefore, to test the hypothesis that a shortened PML is associated with the development of Carpentier’s functional classification Type I MR in AF patients, especially in those without LV remodeling.

**Methods**

**Study Population**

This study was a retrospective analysis of 96 AF patients who were referred for pulmonary vein isolation or cardioversion at Kobe University Hospital between February 2016 and September 2017. Patients were excluded from enrolment in the study if they met any of the following...
This study was approved by the local institutional ethics committee (No. 180112).

**Echocardiographic Examination**

All transesophageal echocardiography (TEE) studies were performed with a commercially available echocardiographic system (ACUSON SC2000; Siemens Medical Solutions, Mountain View, CA, USA). Transthoracic echocardiography (TTE) studies were performed with other commercially available echocardiographic systems within 5 days of criteria: (1) LV ejection fraction (LVEF) <50%; (2) previous history of open-heart surgery; (3) serious renal dysfunction defined as glomerular filtration rate <30 mL/min/1.73 m²; (4) uncontrolled hypertension >180/100 mmHg; (5) more than moderate aortic valve disease; and (6) major cause of MR other than Carpentier’s functional classification Type I. We also excluded patients with Carpentier’s functional classification Type I MR who had PML hamstringing, in order to exclude the effect on the development of MR of the tip of the PML tethering towards the LV posterior wall.

Figure 1. Representative cases of a patient with sinus rhythm without mitral regurgitation (MR) and an atrial fibrillation (AF) patient with significant MR, showing that AF patients with significant MR are more frequently observed with a posterior mitral leaflet (PML) that is shorter than the anterior mitral leaflet (AML).

Figure 2. Assessment of mitral valve geometric parameters by 3D transesophageal echocardiography. Mitral annulus area, anterior (AML) area and posterior mitral leaflet (PML) area were determined in this study.
the MV and its orientation and dimensions in the image are detected first to form a region of interest, within which key landmarks such as trigones and commissures as well as the annulus and leaflet free edges can be detected, after which an average surface model of the anterior and posterior leaflets is fitted to the landmarks. The shapes of these contours are then altered to match the atrial side of the leaflets in the image. To facilitate automated computation of complex measurements, the surface model returned by eSie Valves™ (Siemens Healthineers, Erlangen, Germany) is represented uniformly. This is established from a landmark-based resampling procedure. Each vertex of the valve surface model is uniquely defined by 2 coordinates: the u-coordinate, tangential to the valve circumference, from anterior to posterior, and the v-coordinate, perpendicular to the valve circumference, from annulus to free edge. Once the MV is modeled, different workflow options are available to confirm the predetermined landmarks and edit the segmented valve (Figure 2). For this study, the mitral annulus area, AML area and PML area were measured, the TEE studies (Xario SSA-660 A; Aplio XG, and ARTIDA; Canon Medical Systems, Tochigi, Japan, or iE 33; Philips Medical Systems, Andover, MA, USA). Digital routine grayscale 2-D cine loops and tissue Doppler cine loops were obtained from 3 consecutive beats with end-expiratory apnea from standard apical and parasternal views. Sector width was optimized to allow for complete myocardial visualization while the frame rate was maximized regardless of heart rate. Standard TTE measurements were obtained in accordance with the current guidelines of the European Association of Cardiovascular Imaging.

**Assessment of 3D MV Geometric Analysis**

3D MV geometric analysis was performed offline using semi-automated valve software (eSie Valves; Siemens Medical Solutions) as previously described in detail. Briefly, 3D digital imaging and communications in medicine data are loaded first, and a mid-systolic frame is chosen for subsequent analysis. The MV is then segmented automatically using a machine-learning algorithm. The position of

| Table 1. Baseline Clinical and Echocardiographic Characteristics | All patients (n=96) | Patients with MR (n=11) | Patients without MR (n=85) | P value |
|---------------------------------------------------------------|-------------------|------------------------|---------------------------|--------|
| **Clinical characteristics**                                  |                   |                        |                           |        |
| Age (years)                                                   | 65.9±9.9          | 70.7±10.8              | 65.6±9.9                  | 0.12   |
| Gender (female) [n (%)]                                       | 34 (35.4)         | 6 (54.5)               | 28 (32.9)                 | 0.142  |
| Body surface area (m²)                                        | 1.72±0.20         | 1.49±0.21              | 1.74±0.19                 | 0.001  |
| Chronic AF [n (%)]                                            | 47 (49.0)         | 11 (100)               | 36 (42.4)                 | <0.001 |
| Paroxysmal AF [n (%)]                                         | 49 (51.0)         | 0 (0)                  | 49 (57.6)                 | <0.001 |
| CHADS2 score                                                  | 1.35±1.31         | 2.18±1.60              | 1.26±1.23                 | 0.041  |
| Congestive heart failure [n (%)]                              | 16 (16.7)         | 8 (72.7)               | 8 (9.4)                   | <0.001 |
| Hypertension [n (%)]                                          | 51 (53.1)         | 6 (54.5)               | 45 (52.9)                 | 0.92   |
| Age (>75 years) [n (%)]                                       | 20 (20.8)         | 5 (45.5)               | 15 (17.6)                 | 0.048  |
| Diabetes mellitus [n (%)]                                     | 20 (20.8)         | 1 (9.1)                | 19 (22.4)                 | 0.28   |
| Stroke / TIA [n (%)]                                          | 13 (13.5)         | 2 (18.2)               | 11 (12.9)                 | 0.46   |
| **Echocardiographic parameters**                              |                   |                        |                           |        |
| LV end-diastolic diameter (mm)                                | 46.7±5.8          | 51.4±7.9               | 46.0±5.2                  | 0.004  |
| LV end-systolic diameter (mm)                                 | 30.5±5.6          | 37.2±7.6               | 29.6±4.7                  | 0.008  |
| LVEF (%)                                                      | 62.8±6.2          | 64.7±6.8               | 62.7±5.7                  | 0.704  |
| Interventricular septum thickness (mm)                        | 10.2±2.3          | 9.2±2.6                | 10.3±2.2                  | 0.138  |
| Posterior wall thickness (mm)                                 | 10.0±1.9          | 9.6±1.5                | 10.1±1.9                  | 0.593  |
| LAVI (mL/m²)                                                  | 50.7±30.0         | 110.4±57.5             | 43.3±16.8                 | <0.0001|
| E (cm/s)                                                      | 79.4±24.6         | 112.2±46.4             | 73.8±17.3                 | 0.008  |
| **3D mitral valve geometric parameters**                      |                   |                        |                           |        |
| AML area (cm²)                                                | 4.6±1.0           | 5.8±1.1                | 4.4±0.9                   | <0.001 |
| PML area (cm²)                                                | 4.8±1.0           | 5.3±1.0                | 4.6±0.9                   | 0.041  |
| Relative AML area                                             | 0.54±0.07         | 0.56±0.08              | 0.54±0.07                 | 0.654  |
| Relative PML area                                             | 0.56±0.09         | 0.51±0.06              | 0.57±0.01                 | 0.002  |
| PML area / AML area                                           | 1.06±0.20         | 0.93±0.19              | 1.08±0.20                 | 0.021  |
| Mitral annulus area (cm²)                                     | 8.48±1.74         | 10.6±1.8               | 8.2±1.5                   | <0.0001|
| A1 length (mm)                                                | 1.34±0.16         | 1.47±0.13              | 1.32±0.16                 | 0.003  |
| A2 length (mm)                                                | 1.91±0.25         | 2.13±0.25              | 1.88±0.24                 | 0.005  |
| A3 length (mm)                                                | 1.26±0.21         | 1.5±0.37               | 1.22±0.16                 | 0.003  |
| P1 length (mm)                                                | 1.21±0.16         | 1.11±0.14              | 1.22±0.16                 | 0.03   |
| P2 length (mm)                                                | 1.24±0.22         | 1.08±0.25              | 1.26±0.21                 | 0.032  |
| P3 length (mm)                                                | 1.29±0.21         | 1.16±0.19              | 1.3±0.21                  | 0.042  |

Data are presented as mean±SD, or n (%). 3D, 3-dimensional; AF, atrial fibrillation; AML, anterior mitral leaflet; E, peak early diastolic mitral flow velocity; EF, ejection fraction; LAVI, left atrial volume index; LV, left ventricular; PML; posterior mitral leaflet; TIA, transient ischemic attack.

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MR With Short PML in AF

Assessment of Severity of MR

MR was quantified in the parasternal long-axis view of TTE by measuring the vena contracta width in the zoom mode at the narrowest portion of the MR jet as it emerges from the orifice. The severity of MR was graded as none or trace (<0.30 cm), mild (0.30–0.69 cm), or severe (≥0.70 cm). More than moderate MR was defined as significant.

Statistical Analysis

Continuous variables are expressed as mean values and standard deviation for normally distributed data, and as the median and interquartile range for non-normally distributed data. Categorical variables are expressed as frequencies and percentages. The parameters of subgroups were compared by Student’s t-test or Mann-Whitney U test as appropriate, and proportional differences were evaluated by Fisher’s exact test or the χ2 test as appropriate. The initial univariate regression analysis to identify univariate associated parameters of significant MR was followed by a multivariate regression model using enter selection. Sequential logistic models were constructed to determine the incremental benefit by using the relative PML area for determining the associations of significant MR over clinical variables including age, gender, LVEF, and LA volume index (LAVI) as well as the mitral annulus area. For all steps, a P value of <0.05 was regarded as statistically significant. The intraclass correlation coefficient was used to determine inter- and intra-observer reproducibility for 3D MV geometric parameters from 20 randomly selected subjects. All analyses were performed with commercially available software (SPSS software...
version 25.0, SPPS Inc., Chicago, IL, USA).

**Results**

**Patients’ Characteristics**
The baseline clinical and TTE characteristics of the 96 AF patients are summarized in Table 1. Their mean age was 66±10 years, 34 patients (35%) were female, and LVEF was 63±6%. Chronic AF was diagnosed in 47 patients (49%) and paroxysmal AF in the remaining 49 patients (51%). Mean CHADS2 score was 1.4±1.3.

**Comparison of Clinical and Echocardiographic Parameters of MR and Non-MR Groups**
The baseline clinical and TTE characteristics of patients in the MR and non-MR groups are summarized in Table 1. The MR group, comprising patients classified as having more than moderate MR, consisted of 11 patients (11%), and the remaining 85 patients (89%) made up the non-MR group. The 2 groups showed similar baseline clinical and echocardiographic characteristics, except for the fact that patients in the MR group were more likely to have a smaller body surface area (1.49±0.21 vs. 1.74±0.19 m², *P*=0.001), higher prevalence of chronic AF (100% vs. 42%, *P*<0.001), higher CHADS2 score (2.2±1.6 vs. 1.3±1.2, *P*<0.001), larger LV dimensions (LV end-diastolic diameter: 51.4±7.9 vs. 46.0±5.2 mm, *P*=0.004 and LV end-systolic diameter: 37.2±7.6 vs. 29.6±4.7 mm, *P*=0.008), larger LAVI (110.4±57.5 vs. 43.3±16.8 mL/m², *P*<0.0001), and a higher transmitral E wave (112.2±46.4 vs. 73.8±17.3 cm/s, *P*=0.008).
Reproducibility of 3D MV Geometric Parameters

The intraclass correlation coefficients for interobserver reproducibility of 3D MV geometric parameters, including the mitral annulus the AML and the PML area, were 0.969 (95% CI: 0.926–0.987), and 0.960 (95% CI: 0.903–0.983), respectively, and the corresponding coefficients for intraobserver reproducibility were 0.969 (95% CI: 0.924–0.987), and 0.967 (95% CI: 0.920–0.986).

Discussion

The findings of this study indicated that a relatively short PML as assessed by 3D-TEE was independently associated with the development of MR in AF patients. Furthermore, in addition to LA dilatation and mitral annulus dilatation, a relatively short PML appears to be a valuable additional parameter in the development of MR in AF patients.

MR in AF Patients

AF can cause mitral annular dilation without LV dysfunction or dilation, which has been recognized by surgeons as the cause of Carpentier Type I MR. The mitral leaflets of AF patients can adapt by compensatory enlargement in response to mechanical stretching resulting from mitral annular dilatation caused by LA remodeling. However, if the mitral annulus dilates beyond the limits of MV leaflet adaptation, it impairs sufficient mitral leaflet co-adaptation and MR can occur as result. Moreover, long-lasting AF causes LA remodeling that also leads to morphological and functional changes in the MV apparatus. It has recently been reported that the development of MR in AF patients is associated with not only mitral annular dilatation caused by LA enlargement, but also with multiple other factors. Machino-Ohtsuka et al reported that, in addition to PML tethering and mitral annular dilatation, a variety of other factors, including a flattened mitral annular saddle shape, mitral annulus contractile dysfunction, and PML tethering, were associated with the development of MR in chronic AF patients and that PML tethering and mitral annular

Figure 6. Patients with severe Carpentier Type I mitral regurgitation (MR) usually undergo mitral ring annuloplasty (A). However, atrial fibrillation (AF) patients with Carpentier Type I MR and a relatively short posterior mitral leaflet (PML) occasionally experience recurrent MR after mitral ring annuloplasty only, because of restricted PML motion in the late stage (B), and such patients may need additional procedures such as posterior mitral valve leaflet augmentation (C).
It was recently reported that geometric change of the PML is associated with significant MR in AF patients without LV remodeling. Ito et al showed by means of 3D-TEE that, in addition to LA remodeling and mitral annular dilatation, the AML was flattened along the mitral annular plane, whereas the PML was bent towards the LV cavity, known as PML hamstringing, in AF patients with significant MR. This functional restriction of the PML has traditionally occurred because of the giant LA that is seen in advanced rheumatic MV disease, and AF patients are also likely to have PML hamstringing in association with severe LA dilatation. Because the purpose of this study was to investigate only the association of a relatively short PML with the development of MR in AF patients, we excluded AF patients with PML hamstringing, which may strongly affect the development of MR. In this study a relatively short PML was associated with the development of MR in AF patients, as well as mitral anulus dilatation. Moreover, PML area was larger but PML length, including P1, P2, and P3, was smaller in the MR group than in the non-MR group. Thus, the transverse extension of the PML caused by transverse dilatation of the mitral annulus rather than by longitudinal shortening of the PML may be associated with the development of MR in AF patients.

The precise mechanism of the occurrence of a relatively short PML in AF patients remains unclear. Several investigators have reported local immunologic inflammatory responses are associated with the LA in AF patients, so a relatively short PML in AF patients may be related to this. Other studies are required to provide pathological evidence for the mechanism of the occurrence of a relatively short PML in AF patients.

Clinical Implications
Symptomatic AF patients with severe Carpentier Type I MR usually undergo mitral ring annuloplasty (Figure 6A). However, AF patients with Carpentier Type I MR and a relatively short PML in the late stage occasionally experience recurrent MR after mitral ring annuloplasty only, because of the restricted PML motion (Figure 6B). Such patients may thus need an additional procedure such as posterior MV leaflet augmentation (Figure 6C). Therefore, the identification of a relatively short PML in AF patients by means of 3D-TEE can be expected to be reliable, and may well have clinical implications for better surgical management of symptomatic AF patients with significant MR.

Study Limitations
This study covered a small number of patients in a single-center retrospective study, so future studies involving larger numbers of patients are required to verify our findings. Another limitation of this study was that the irregular rhythm of AF can affect the evaluation of MR severity. In addition, the assessment of MR severity in this study was performed by a semiquantitative method not quantitative method such as regurgitant volume, regurgitant fraction, or effective regurgitant orifice area. Finally, MR in patients with AF may change according to hemodynamics. However, all patients in this study were in a clinically stable condition at the time of TTE and TEE studies.

Conclusions
In addition to mitral annulus dilatation, a relatively short PML plays an important role in the development of MR in AF patients. The assessment of a relatively short PML by means of 3D-TEE is thus a valuable additive parameter for better surgical management of AF patients with significant MR.

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