Test-retest reproducibility of $^{[11}C$-L-deprenyl-D$_2$ binding to MAO-B in the human brain

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Abstract

Background: $^{[11}C$-L-deprenyl-D$_2$ is a positron emission tomography (PET) radioligand for measurement of the monoamine oxidase B (MAO-B) activity in vivo brain. The estimation of the test-retest reproducibility is important for accurate interpretation of PET studies.

Results: We performed two $^{[11}C$-L-deprenyl-D$_2$ scans for six healthy subjects and evaluated the test-retest variability of this radioligand. MAO-B binding was quantified by two tissue compartment model (2TCM) with three rate constants ($K_1$, $k_2$, $k_3$) using metabolite-corrected plasma radioactivity. The $\lambda k_3$ defined as $(K_1/k_2) \times k_3$ was also calculated. The correlation between MAO-B binding and age, and the effect of partial volume effect correction (PVEc) for the reproducibility were also estimated. %difference of $k_3$ was 2.6% (medial frontal cortex) to 10.3% (hippocampus), and that of $\lambda k_3$ was 5.0% (thalamus) to 9.2% (cerebellum). Mean %difference of all regions were 5.3 and 7.0% in $k_3$ and $\lambda k_3$, respectively. Intraclass correlation coefficient (ICC) of $k_3$ was 0.78 (hippocampus) to 0.98 (medial frontal cortex), and that of $\lambda k_3$ was 0.78 (hippocampus) to 0.95 (thalamus). Mean ICC were 0.94 and 0.90 for $k_3$ and $\lambda k_3$, respectively.

Conclusions: The present results indicate that $k_3$ and $\lambda k_3$ of $^{[11}C$-L-deprenyl-D$_2$ are reliable parameters for test-retest reproducibility with healthy subjects both before and after PVEc. The studies with patients of larger sample size are required for further clinical applications.

Keywords: Age effect, $^{[11}C$-L-deprenyl-D$_2$, Monoamine oxidase B, Partial volume effect correction, Positron emission tomography, Test-retest variability

Background

Monoamine oxidase (MAO) is an enzyme of deamination of monoamine and exists in two isoforms, MAO-A and MAO-B. MAO-B is considered as a major enzyme in dopamine metabolism in the human brain, and MAO-B inhibitors are used for the treatment of Parkinson’s disease to increase the dopamine level [1]. For Alzheimer’s disease (AD), several studies reported the upregulation of MAO-B expression related to the neuroinflammatory process in the glia cells [2–6]. So, inhibition of MAO-B is expected to have beneficial effects in AD by reducing neurodegenerative processes.

$^{[11}C$-L-deprenyl-D$_2$ is a positron emission tomography (PET) radioligand for measurement of the MAO-B activity in the brain [7]. This radioligand was used for many PET studies to evaluate MAO-B inhibitors’ occupancy [8, 9], pathology of AD [10–12], amyotrophic lateral sclerosis (ALS) [13], traumatic brain injury [14], and epilepsy [15–17]. In addition to the clinical studies, $^{[11}C$-L-deprenyl-D$_2$ showed good result reproducibility in a test-retest protocol [18].

Recently, we reported the brain occupancy of MAO-B using $^{[11}C$-L-deprenyl-D$_2$ after administration of a
MAO-B inhibitor, sembragiline, in controls and patients with AD [9]. Although the good reproducibility of $^{11}$C-L-deprenyl-D$_2$ has already been reported, confirmation in test-retest variability studies by using identical protocol settings, including radioligand production and PET machine, is helpful for accurate interpretation of occupancy. Additionally, age effect of $^{11}$C-L-deprenyl-D$_2$ should be estimated since an increase of MAO-B expression has been reported in elderly subjects by postmortem [19] and in vivo PET [20] studies. The partial volume effect (PVE) should be also considered in the PET studies for aged subjects or AD patients with brain atrophy [21, 22].

In this study, we focused on three issues. First, we evaluated the test-retest variability of $^{11}$C-L-deprenyl-D$_2$ in the healthy subjects who were scanned twice. Second, the correlation between MAO-B activity and age was estimated. Finally, the effect of partial volume effect correction (PVEc) for the reproducibility was also estimated.

**Methods**

**Subjects**

Six healthy volunteers (age range, 21–62 years; mean ± SD, 39.0 ± 17.0; four males, two females) were enrolled in the study. None had a history of present or past psychiatric, neurological, or somatic disorders, or alcohol or drug-related problems. They took no medication at the time of the study. After thorough explanation of the study, written informed consent was obtained from all participants. The study was approved by the Regional Ethical Review Board in Stockholm, Sweden, and the Radiation Safety Committee at the Karolinska University Hospital Solna in Stockholm, Sweden.

**PET procedures**

$^{11}$C-L-deprenyl-D$_2$ was prepared by N-methylation of the desmethyl l-deprenyl-D$_2$ precursor using $^{11}$C-methyl triflate as previously reported [9]. PET scans were carried out with the ECAT Exact HR 47 (Siemens/CTI, Knoxville, TN, USA), with an in-plane and an axial resolution of 3.6 and 4.0 mm at full width at half maximum (FWHM), respectively. A head fixation system with an individual plaster helmet was used. A 5-min transmission scan was performed using three rotating $^{68}$Ge rod sources. Dynamic PET scan was performed for 63 min (10 s × 9, 15 s × 2, 20 s × 3, 30 s × 4, 1 min × 4, 3 min × 4, 6 min × 7) after intravenous bolus injection of $^{11}$C-L-deprenyl-D$_2$. Injected radioactivity was 299–520 MBq (419 ± 68 MBq), which were adjusted by body weight. Specific radioactivity was 104–341 GBq/μmol (179 ± 80 GBq/μmol) at the time of injection. Injected mass was 0.24–0.77 μg (0.50 ± 0.18 μg). Two PET scans were performed for each subject in the morning and in the afternoon on the same day.

**Arterial blood sampling**

Arterial blood was collected continuously for 10 min using an automated blood sampling system at a speed of 5 mL/min. Arterial blood was also drawn manually 1, 2, 4, 6, 8, 10, 15, 20, 30, 45, and 60 min after the injection for measurement of radioactivity in whole blood and plasma. The parent fraction of the radioligand was determined using a reversed-phase high-performance liquid chromatography (HPLC) method at 4, 10, 20, 30, 45, and 60 min. Plasma input function was defined as radioactivity of plasma multiplied by the percentage of unchanged radioligand.

**Data analysis**

PET images were reconstructed using the standard filtered back projection with a 2-mm Hanning filter, a zoom factor of 2.17, and a 128 × 128 matrix, and were corrected for attenuation and scatter. T1-weighted magnetic resonance imaging (MRI) was performed using a 1.5-T Siemens MAGNETOM Avanto for definition of anatomical brain regions. PET images were reconstructed using the SPM5 segmentation algorithm in MATLAB (Wellcome Trust Centre for Neuroimaging, London, UK; The MathWorks, Inc., Natick, MA, USA). Regions of interest (ROI) were defined as the cerebellum, hippocampus, lateral frontal cortex, lateral occipital cortex, lateral parietal cortex, lateral temporal cortex, medial frontal cortex, putamen, and thalamus using the Anatomical Automatic Labeling (AAL) template [23]. GM masking was applied to the AAL template. All MRIs and ROIs were co-registered to summed PET images with the mutual information algorithm using SPM5. Regional radioactivity was calculated for each frame, corrected for decay, and plotted vs. time.

MAO-B binding of $^{11}$C-L-deprenyl-D$_2$ was quantified by two tissue compartment model (2TCM) with three rate constants ($K_1$, $k_2$, $k_3$) using metabolite-corrected plasma radioactivity as the input function. $k_4$ was set as 0 according to the assumption of irreversible binding of $^{11}$C-L-deprenyl-D$_2$ [7, 18]. Blood volume was fixed at 5%. The $\lambda k_3$ defined as $(K_1/k_2) \times k_3$ was also calculated. These analyses were performed using the PMOD 3.4 software package (PMOD Group, Zurich, Switzerland).

**PVEc**

All PET data were corrected for PVE according to the method reported by Müller-Gärtner et al. [21]. In short, this PVEc corrects for spillover between GM and WM, and between GM and CSF using the segmented MR images. By assuming that the radioligand binding in WM is perfectly homogenous, every WM-voxel were replaced...
by an average value derived from an isolated proportion of WM at the centrum semiovale [22].

### Statistics

The test-retest variability of MAO-B binding as \( k_3 \) and \( \lambda k_3 \) was expressed by the absolute difference between the first and second PET scans (PET1 and PET2) relative to the mean of the two values according to the following equation [24, 25]:

\[
\text{%difference} = \left| \frac{\text{PET1} - \text{PET2}}{((\text{PET1} + \text{PET2})/2)} \right| \times 100
\]

PET1 and PET2 are the parameters \((k_3 \text{ or } \lambda k_3)\) of first and second PET scans, respectively.

Intraclass correlation coefficient (ICC) was also calculated by:

\[
\text{ICC} = \frac{(\text{MSBS} - \text{MSWS})}{(\text{MSBS} + \text{MSWS})}
\]

MSBS is the mean square of between subject, and MSWS is the mean square of within subject. The correlation between MAO-B binding as \( k_3 \) or \( \lambda k_3 \) and age was estimated using the Pearson correlation coefficient.

The effect of PVEc was estimated by the %change of before and after PVEc of all parameters, \( K_1, k_2, k_3, \) and \( \lambda k_3 \):

\[
\text{%change} = \left( \frac{\text{after PVEc} - \text{before PVEc}}{\text{before PVEc}} \right) \times 100
\]

In both analysis of age effect and PVEc, average values of PET1 and PET2 were used. Finally, the test-retest variability of after PVEc was estimated as same way as before PVEc.

These statistical analyses were performed using R 3.3.2 (The R Foundation, Vienna, Austria).

### Results

#### Test-retest variability

Mean and SD values of six subjects in PET1 and PET2, mean and range of %differences, and ICC in all regions are shown in Table 1. %difference of \( k_3 \) was 2.6% (medial frontal cortex) to 10.3% (hippocampus), and that of \( \lambda k_3 \) was 5.0% (thalamus) to 9.2% (cerebellum). Mean %difference of nine regions were 5.3% and 7.0% in \( k_3 \) and \( \lambda k_3 \), respectively. All regions showed variability below 10%, except the hippocampus in \( k_3 \) (10.3%). ICC of \( k_3 \) was 0.78 (hippocampus) to 0.98 (medial frontal cortex), and that of \( \lambda k_3 \) was 0.78 (hippocampus) to 0.95 (thalamus). Mean ICC of nine regions were 0.94 and 0.89 in \( k_3 \) and \( \lambda k_3 \), respectively.

#### Age effect

The Pearson correlation coefficient and \( p \) value between \( k_3 \) or \( \lambda k_3 \) and age in all regions are shown in Table 2. The highest positive correlation was observed in the hippocampus (\( r = 0.75 \) in \( k_3 \) and 0.76 in \( \lambda k_3 \); Fig. 1a, b). Regardless, both results were not statistically significant (\( p = 0.08 \) and \( p = 0.08 \), respectively).

#### PVEc

After PVEc, \( K_1 \) values increased as 36.9 to 62.7% according to the age (Fig. 2). %change of \( \lambda k_3 \) was 23.5 to 37.0% and also correlated with age. Compared to \( K_1 \) and \( \lambda k_3 \), \( k_2 \) and \( k_3 \) showed only small changes after PVEc (11.6 to 15.4% and \(-1.3 \) to 5.5%, respectively).

Mean and SD values of six subjects in PET1 and PET2, mean and range of %differences, and ICC after PVEc in all regions are shown in Table 3. Mean %difference of nine regions were 5.6 and 7.2% in \( k_3 \) and \( \lambda k_3 \), respectively. Mean ICC of nine regions were 0.92 and 0.90 in \( k_3 \) and \( \lambda k_3 \), respectively. These values were almost the same as those before PVEc.

### Table 1

| Region             | \( k_3 \) | \( \lambda k_3 \) | %dif | Range | ICC  | %dif | Range | ICC  |
|--------------------|----------|-----------------|------|-------|------|------|-------|------|
|                    | PET1 | SD   | PET2 | SD   | Mean | Range | Mean | SD   |
| Cerebellum         | 0.051 | 0.011 | 0.051 | 0.012 | 0.07–11.1 | 0.96 | 0.143 | 0.030 | 0.140 | 0.031 | 0.92 | 5.9–15.4 | 0.90 |
| Hippocampus        | 0.103 | 0.023 | 0.108 | 0.017 | 0.02–20.6 | 0.78 | 0.288 | 0.028 | 0.285 | 0.047 | 6.4 | 1.0–17.6 | 0.78 |
| Lateral frontal cortex | 0.067 | 0.014 | 0.067 | 0.013 | 0.3–7.2 | 0.92 | 0.185 | 0.023 | 0.184 | 0.033 | 6.0 | 2.4–14.2 | 0.91 |
| Lateral occipital cortex | 0.060 | 0.013 | 0.061 | 0.013 | 6.4 | 1.0–15.1 | 0.92 | 0.175 | 0.024 | 0.170 | 0.030 | 8.0 | 3.0–15.0 | 0.86 |
| Lateral parietal cortex | 0.063 | 0.012 | 0.064 | 0.012 | 3.7 | 1.4–7.7 | 0.97 | 0.180 | 0.027 | 0.182 | 0.035 | 7.2 | 2.5–12.1 | 0.91 |
| Lateral temporal cortex | 0.065 | 0.015 | 0.063 | 0.015 | 5.9 | 0.1–13.7 | 0.95 | 0.201 | 0.029 | 0.199 | 0.041 | 8.3 | 2.2–20.0 | 0.86 |
| Medial frontal cortex | 0.068 | 0.012 | 0.067 | 0.011 | 2.6 | 1.1–4.6 | 0.98 | 0.175 | 0.019 | 0.175 | 0.026 | 5.7 | 2.8–10.1 | 0.89 |
| Putamen            | 0.087 | 0.019 | 0.085 | 0.016 | 5.4 | 3.2–7.6 | 0.96 | 0.323 | 0.051 | 0.331 | 0.072 | 7.4 | 3.0–10.5 | 0.91 |
| Thalamus           | 0.083 | 0.017 | 0.082 | 0.017 | 4.2 | 0.1–9.4 | 0.97 | 0.306 | 0.047 | 0.308 | 0.059 | 5.0 | 1.5–8.6 | 0.95 |
Table 2 The Pearson correlation coefficient and p value between age and parameters in all regions of $k_3$ and $\lambda k_3$

| Region                | $k_3$  | p     | $\lambda k_3$ | p     |
|-----------------------|--------|-------|---------------|-------|
| Cerebellum            | 0.58   | 0.23  | 0.56          | 0.25  |
| Hippocampus           | 0.75   | 0.08  | 0.76          | 0.08  |
| Lateral frontal cortex| 0.65   | 0.17  | 0.73          | 0.10  |
| Lateral occipital cortex | 0.66  | 0.16  | 0.59          | 0.22  |
| Lateral parietal cortex | 0.70  | 0.13  | 0.64          | 0.18  |
| Lateral temporal cortex | 0.69  | 0.13  | 0.72          | 0.10  |
| Medial frontal cortex  | 0.58   | 0.22  | 0.66          | 0.15  |
| Putamen               | 0.67   | 0.15  | 0.75          | 0.09  |
| Thalamus              | 0.69   | 0.13  | 0.63          | 0.18  |

**Discussion**

In this study, the test-retest variability of $[11C]$-L-deprenyl-D$_2$ was estimated using healthy subjects. Mean of absolute %difference in nine regions of $\lambda k_3$ was 7.0%, indicating good reproducibility. The test-retest variability of $\lambda k_3$ using %difference (not absolute difference) by Logan et al. was previously reported as $-2.84 \pm 7.07\%$ [18]. The same calculation of our data yielded $-1.1 \pm 8.3\%$, indicating similar variability. ICC values were high in all regions, except in the hippocampus which was relatively low (0.78). It also indicated good reproducibility of $[11C]$-L-deprenyl-D$_2$. Our research group recently reported the brain occupancy of MAO-B using $[11C]$-L-deprenyl-D$_2$ after administration of a MAO-B inhibitor—semmagiline [9]. The study reported that oral administrations of 1–5 mg semmagiline induced near-maximal inhibition of brain MAO-B, and MAO-B occupancy was correlated with the plasma concentration of semmagiline in patients with AD. The good test-retest reproducibility of the present study using same procedure of $[11C]$-L-deprenyl-D$_2$ preparation and same PET camera corroborates the findings of our previous study.

Although $\lambda k_3$ is generally considered to be a more stable outcome measure than $k_3$ [7, 18], $k_3$ showed similar %difference as $\lambda k_3$ (5.3 vs 7.0%) in the present study. $k_3$ values also showed better ICC than those of $\lambda k_3$ (mean value, 0.94 vs 0.89). These findings indicate that $k_3$ may be independently used for further studies such as comparison between patients and healthy controls or target occupancy of MAO-B inhibitors. Obvious regional differences of reproducibility were only observed in the hippocampus. The reason of low reproducibility in the hippocampus is not clear, but one possibility is that its high $k_3$ value (the highest among all regions) may have induced a large variability.

In this study, two PET measurements were performed in 1 day, in the morning and afternoon. Several studies suggested that dopamine system was affected by the circadian rhythm [26–28]. Especially, one rodent study reported that MAO-A expression was regulated by the clock-component gene [29]. However, our result did not show the relation between the MAO-B binding and the time of PET measurements.
A moderate age effect on $\lambda k_3$ values was observed in all regions. The degree of increase (6.3% per decade) was similar as the previously reported value by Fowler et al., at 7.1% per decade [20]. One postmortem study also reported increasing of MAO-B protein in the human brain according to age [19]. Our PET study confirmed both findings of postmortem and in vivo human brain studies. Among all regions, the hippocampus showed the highest correlation with age effect although it did not reach statistical significance and the reproducibility was relatively low as discussed above. Since the hippocampus is thought to be especially impacted in AD [30, 31], the present findings suggest the increase of MAO-B activity may have an important role about the pathology of AD.

PVE should be considered in PET studies when brain atrophy is observed in aged subjects or patients with disorders such as AD. Additionally, PVE is larger using a low resolution PET camera than a high resolution one. This study included elderly subjects and was conducted using relatively low resolution PET camera system compared to recent PET systems like the high resolution research tomograph (HRRT) with 1.5 mm FWHM [32]. In the present study, %change of $K_1$ after PVEc was correlated with age. It indicates that the brain of aged subjects was more affected by the PVE compared to younger subject due to the brain atrophy. Meanwhile, $k_2$ and $k_3$ did not show any clear change after PVEc. $\lambda k_3$ was also moderately affected by PVEc and correlated with age since it is partially determined by $K_1/k_2$. Nevertheless, although the value itself of $\lambda k_3$ was increased in aged subjects, test-retest variability of $\lambda k_3$ did not change after PVEc. This indicates that PVEc can reliably keep reproducibility even in the case of elderly subjects with brain atrophy.

There are several imitations in this study. Although only six subjects were included and it is relatively small sample size, the number were similar as previous test-retest studies about $[^{11}\text{C}]-\text{L-deprenyl-D}_2$ by Logan et al. ($n = 5$) [18] and other PET radioligands ($n = 6–8$) [25, 33]. However, the studies about age effect included larger number generally [20, 34, 35]. So, the present result about the age effect might be preliminary. Additionally, only healthy control subjects were included in this study. It is difficult to extrapolate our findings about PVEc to AD patients because the elderly ones showed slight atrophy but not pathological. To more accurately estimate the effects of PVEc, further studies with AD patients and aged control subjects who showed strong atrophy will be needed.

**Conclusions**

The present results indicate that $k_3$ and $\lambda k_3$ of $[^{11}\text{C}]-\text{L-deprenyl-D}_2$ are reliable parameters for test-retest reproducibility with healthy subjects both before and after PVEc. As the number of subjects was relatively small and only healthy subjects were included, the studies with patients of larger sample size are required for further clinical applications.

**Abbreviations**

2TCM: Two tissue compartment model; AAL: Anatomical Automatic Labeling; AD: Alzheimer’s disease; ALS: Amyotrophic lateral sclerosis; CSF: Cerebrospinal fluid; FWHM: Full width at half maximum; GM: Grey matter; HRRT: High resolution research tomograph; ICC: Intraclass correlation coefficient; MAO: Monoamine oxidase; MRI: Magnetic resonance image; MSBS: Mean square of between subject; MSWS: Mean square of within subject; PET: Positron emission tomography; PMV: Partial volume effect; PVE: Partial volume effect correction; ROI: Regions of interest; WM: White matter

**Acknowledgements**

We thank all members of the Karolinska Institutet PET Centre for assistance with the PET experiments. RSM was recipient of a post doc fellowship (CNPq-23364/2014-7).

**Funding**

This work was partially supported by GE Healthcare Ltd., UK.
Authors’ contributions
PS, AT, and CH designed the study and wrote the protocol. PS and SN conducted the PET experiment. RA, PS, AT, and RSM analyzed the data. RA wrote the first draft of the manuscript. All authors read and approved the final manuscript.

Competing interests
The authors declare that they have no competing interests.

Consent for publication
Not applicable

Ethics approval and consent to participate
The study was approved by the Regional Ethical Review Board in Stockholm, Sweden, and the Radiation Safety Committee at the Karolinska University Hospital in Solna in Stockholm, Sweden. After thorough explanation of the study, written informed consent was obtained from all participants.

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Received: 24 April 2017 Accepted: 9 June 2017

Published online: 20 June 2017

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