Advances in stereotactic navigation for pelvic surgery

A. R. Wijsmuller1,2 · L. G. C. Romagnolo3 · V. Agnus1 · C. Giraudeau4 · A. G. F. Melani3,5 · B. Dallemagne1 · J. Marescaux1

Received: 8 June 2017 / Accepted: 23 October 2017 / Published online: 6 December 2017
© The Author(s) 2017. This article is an open access publication

Abstract

Background Stereotactic navigation could improve the quality of surgery for rectal cancer. Critical challenges related to soft tissue stereotactic pelvic navigation include the potential difference in patient anatomy between intraoperative lithotomy and preoperative supine position for imaging. The objective of this study was to determine the difference in patient anatomy, sacral tilt, and skin fiducial position between these different patient positions and to investigate the feasibility and optimal set-up for stereotactic pelvic navigation.

Methods Four consecutive human anatomical specimens were submitted to repeated CT-scans in a supine and several degrees of lithotomy position. Patient anatomy, sacral tilt, and skin fiducial position were compared by means of an image computing platform. In two specimens, a 10-degree wedge was introduced to reduce the natural tilt of the sacrum during the shift from supine to lithotomy position. A simulation of laparoscopic and transanal surgical procedures was performed to assess the accuracy of the stereotactic navigation.

Results An up-to-supracentimetric change in patient anatomy was noted between different patient positions. This observation was minimized through the application of a wedge. When switching from supine to another position, sacral retroversion occurred independent of the use of a wedge. There was considerable skin fiducial motion between different positions. Accurate stereotactic navigation was obtained with the least registration error (1.9 mm) when the position of the anatomical specimen was registered in a supine position with straight legs, without pneumoperitoneum, using a conventional CT-scan with an identical specimen positioning.

Conclusion The change in patient anatomy is small during the sacral tilt induced by positional changes when using a 10-degree wedge, allowing for an accurate stereotactic surgical navigation. This opens up new promising opportunities to increase the quality of surgery for rectal cancer cases where it is difficult or impossible to identify and dissect along the anatomical planes.

Keywords Surgery · Computer-assisted · Stereotaxis techniques · Neuronavigation · Surgical procedures · Operative · Anatomy · Rectal neoplasms
Introduction

Surgical navigation was developed by neurosurgeons who integrated medical imaging and stereotaxy [1]. It was reported to increase the safety and to minimize the invasiveness of surgical procedures by acting as a guidance tool using tracked surgical instruments in conjunction with preoperative images. It helps the surgeon to identify anatomical structures, which should be targeted or avoided. These systems are currently mainly used in brain, skull base, and vertebral surgery, and they have proven to be an essential adjunct to surgical procedures where anatomical landmarks are obscured and cannot be used for topographic orientation [2]. It could improve the quality of surgery for rectal cancer as shown when used in other contexts.

Recently, the performance of stereotactic navigation for minimally invasive transanal rectal surgery has been reported [3, 4]. Since anatomical structures at risk during rectal surgery are fixed retroperitoneally, they seem to be less affected by pneumoperitoneum and respiratory movements as compared to upper abdominal organs. However, pelvic surgery is associated with additional challenges as compared to surgical navigation in other context such as neurosurgery and orthopedic surgery. Rectal surgery is performed in patients with variable degrees of lithotomy, a position that is different from the supine position used for acquisition of preoperative imaging. This positional change could alter the patient anatomy and subsequently render stereotactic pelvic navigation using preoperative imaging inaccurate. Additionally, the motion of the skin reference points with their fiducial markers by means of positional change can hamper patient position registration in the operating room (OR) to begin with.

The objective of this study was to determine the difference in patient anatomy, sacral tilt, and fiducial marker position between these different patient positions and to investigate the feasibility and optimal set-up for stereotactic pelvic navigation.

Materials and methods

Imaging human anatomical specimens

Four consecutive experimental sessions were performed with four fresh-frozen human male anatomical specimens. These human anatomical specimens were submitted to repeated CT-scans at IHU (Institute of Image-Guided Surgery, University of Strasbourg, scanning technique is provided in supplementary text) to analyze the impact of

Fig. 1 Different patient’s positions were investigated: supine, straight legs (A); Supine, hip abduction 60° (B); Hip flexion 45°, hip abduction 70° (C); Hip flexion 90°, hip abduction 80° (D); sagittal view without wedge (E); sagittal view with 10-degree wedge (F). Pneumoperitoneum as variable is not shown in this figure
various positions and pneumoperitoneum (Fig. 1; Table 1) on the change in patient anatomy, sacral tilt, and skin fiducials position. The upper and lower extremities of the specimens were removed with the proximal parts of the shafts of the humerus and femur still intact on each side. It allowed the acquisition of CT-scan images with the hip in several degrees of flexion, which is not realizable with conventional patients without limb amputations due to the width of the scanning tunnel. Hip flexion was generated by increasing/decreasing the tension on a string fixed around the femoral shaft and the neck and/or around the shoulders of the specimen (Fig. 1). Hip abduction was generated with a wedge placed between the femoral shafts. The angle of hip flexion/abduction was measured by means of a digital goniometer. Human anatomical specimen temperature was around room temperature at 20 °C.

In stereotactic navigation, it is essential to obtain a perfect patient position registration in the OR by means of the navigation system. To do so, skin reference points are marked by means of radiopaque fiducials during preoperative CT-scanning, and these fiducials are left in place intraoperatively. Subsequently, after uploading these preoperative CT-scan images to the navigation system, the position of the patient can be registered via recognition of the fiducials using the optics of the navigation system. After this registration, the patient is tracked by a patient tracker which is fixed to the patient or to the operating table. Surgical instruments are tracked by an instrument tracker which is fixed to the instrument allowing the position of the tip of the instrument to be determined and visualized in the navigation scans. In these human anatomical specimens, a total of 12–18 skin reference points were marked with fiducials which were placed and fixed by means of sutures along the anterior bony landmarks of the pelvis and in between, assuming that skin motion at the level of the bony landmarks was the least. Bony landmarks included the anterior superior iliac spine and the pubic bone.

In the first two sessions, a 12 mmHg pneumoperitoneum induced through a 12 mm infra-umbilical trocar, was an additional variable. In the last two sessions, a forced sacral tilt was induced aiming at a reduction in the natural tilt of the sacrum during the shift from a supine to a lithotomy position, which was noted in the first two sessions. This was induced by a 10-degree wedge placed under the pelvis. The wedge was made from low-density foam, a material used to immobilize and reposition the body for radiation therapy.

### Image computing platform

To determine the change in patient anatomy, sacral tilt, and skin fiducial position, all CT data sets were edited. Predeetermined anatomical landmarks (Table 2) and the center of

| Experimental sessions 1 and 2 | Experimental sessions 3 and 4* |
|-------------------------------|--------------------------------|
| I Supine, legs straight†, no pneumoperitoneum | I Supine, legs straight†, no pneumoperitoneum |
| II Supine, legs straight†, pneumoperitoneum | II Supine, hip abduction 60°, no pneumoperitoneum |
| III Hip flexion 90°, hip abduction 80°, pneumoperitoneum‡ | III Hip flexion 45°, hip abduction 70°, no pneumoperitoneum‡ |
| IV Hip flexion 90°, hip abduction 80°, no pneumoperitoneum‡ | IV Hip flexion 90°, hip abduction 80°, no pneumoperitoneum‡ |

*These scans were performed with or without a 10-degree wedge. A total of 4–8 scans were obtained per human anatomical specimen
†Hip adduction
‡Hip flexion: angle between femur axis and horizontal axis of the operation table

### Table 1

| Position pelvic organs | Sacral tilt |
|------------------------|------------|
| P1 Most distal part ureter just before entering bladder, right side | S1 Distal tip sacrum |
| P2 Most distal part ureter, just before entering bladder, left side | S2 Ventral, upper edge foramen S1, right side |
| P3 Upper most cranial edge bladder | S3 Ventral, upper edge foramen S1, left side |
| P4 Lower most caudal edge prostate where urethra exists* | S4 Upper midline ventral rim sacral promontory |
| P5 Most cranial tip seminal vesicle, right side | S5 Ventral, upper edge foramen S2, right side |
| P6 Most cranial tip seminal vesicle, left side | S6 Ventral, upper edge foramen S2, left side |

*in one anatomical specimen the most caudal edge of the prostate could not be identified. Therefore, in this case marker P4 was placed at an anatomical landmark consisting of a calcification in the prostate that could be identified in all scans.
Markers were manually placed in the center of the skin fiducials in each CT-scan by using an image computing platform (3D Slicer) (B). The other markers S1-6 (C) and P1-6 (D) were placed at the anatomical landmarks as depicted in Table 2.

The sacral tilt angle is defined as the angle between the plane made up by S3–S5 and the vertical plane.

- Patient anatomy: distances between the most centrally located bony S4 landmark and the six P1-6 points (Fig. 2D; Table 2).
- Sacral tilt angle: the angle of the plane between S3–S4–S5 and the vertical plane (Figs. 2C, 3).
- Skin fiducial position: distances between the most centrally located bony S4 landmark and the markers placed in the center of skin fiducials (Fig. 2B).

To test whether the mean sacral tilt angle changes between different positions, paired T-tests were performed to compare different positions. To test whether a 10-degree wedge influences the sacral tilt angle variation, a Fisher’s test was performed comparing the sacral tilt angle variation with and without the 10-degree wedge for different positions. To test whether a 10-degree wedge influences the patient anatomy, for each of the 6 distances (P1-6 to S4), the difference within variance was determined when using the 10-degree wedge as compared to the situation when no wedge was used.

**Laparoscopic and transanal stereotactic navigation**

Alongside conventional CT-scans, a T2-weighted MRI scan and a C-arm CT-scan were also obtained during all tests for at least one position (the scanning technique is provided in a supplementary text). The MRI could be uploaded to the navigation system and fused with the scan used for registration in transanal navigation. At the final stage of each session, C-arm CT-scans were performed in a hybrid OR, and were used to register the position of the specimen alongside registration with conventional CT-scans in real-time. Since these C-arm CT-scans provide limited soft tissue resolution, conventional CT or MRI data sets were fused for transabdominal and transanal stereotactic navigation, respectively.

Each session was concluded with several simulations of laparoscopic and transanal surgery guided by means of stereotactic navigation (StealthStation® S7 surgical navigation system, Medtronic Inc.; brain software). Three additional 5 mm trocars were introduced: 2 trocars in the right
midclavicular line and 1 trocar in the left midclavicular line. Registration of the anatomical specimen position was performed with conventional CT data sets and with an intraoperative real-time C-arm CT-scan, in order to compare their accuracy. The patient tracker was fixed to the operating table adjacent to the pelvis or to the iliac bone at the level of the left anterior superior iliac spine in the first two and last two sessions, respectively. An MRI or conventional CT data set could be fused to navigate during a transanal or laparoscopic surgery in case of registration with C-arm CT-scan with low soft tissue resolution. Key anatomical landmarks were determined to test the navigation precision. The origin of the inferior mesenteric artery, the distal end of the aortic bifurcation and the tip of the promontory in laparoscopy and the exit point of the proximal urethra from the prostate in a transanal approach were identified surgically with an optical tracked instrument and correspondence on the navigation screen was evaluated.

Results

A total of 24 conventional CT-scans were obtained, including 8 scans in the first two sessions and 16 scans in the last two experimental sessions of which 8 scans without and 8 scans with a 10-degree wedge. The global repositioning accuracy for the repeated placement of S1-6 markers in one scan three times was excellent with a mean displacement of 0.7 mm with a standard deviation 0.3 mm ensuring consistent placement.

Patient anatomy

An up-to-supracentimetric change in patient anatomy was noted between different positions for all human anatomical specimens. This observation was minimized through the application of a wedge (Fig. 4). For the third and fourth test, the change in patient anatomy was determined with and without a 10-degree wedge (Supplementary Table 1). For human anatomical specimen 3, Fisher’s test (with a 95% confidence) showed that there was a significant difference within variance for four distances (P2–S4, P3–S4, P5–S4, P6–S4) when using the 10-degree wedge as compared to when no wedge was used. Another Fisher’s test showed a significant difference for only one distance (P4–S4) for human anatomical specimen 4. The boxplots depicted in Fig. 4 illustrate this, having a relative smaller width when using the 10-degree wedge as compared to when no wedge was used.

Fig. 4 The distances between S4 and the six points, P1-P6, are depicted for the 3rd human anatomic specimen with (A) or without the wedge (B). The majority of the boxplots show a relative smaller width when using the 10-degree wedge as compared to when no wedge is used.

Sacral tilt

As compared to the supine position with straight legs, all other configurations result in an increase in the sacral tilt angle as depicted in Tables 3. With a 60-degree hip abduction, the sacrum already retroverts, up to more than 2 degrees. It also seems that pneumoperitoneum induction results in a decrease in sacral tilt. A paired T-test (with a 95% confidence) comparing the mean angle of sacral tilt in a supine position with straight legs with a 90-degree hip flexion position showed a significant difference. Another paired T-test comparing the mean angle of sacral tilt in a supine position with straight legs with a 60-degree hip abduction position, showed a significant difference. A Fisher’s test showed a significant difference when comparing the sacral tilt variation with and without a 10-degree wedge. For the third experimental session, the wedge resulted in more
variations. In contrast, it resulted in fewer variations for the fourth session.

### Skin fiducial position

As expected, displacement of skin fiducials was significantly impacted by pneumoperitoneum induction, rendering it useless in the perspective of optical navigation. This observation led to the abandonment of the method in the last two experiments. The distances between S4 and each individual skin fiducial were determined for the last two human anatomical specimens and are depicted in Supplementary tables 2–5. The standard deviation for these distances in the third session ranged from 0.4 to 2.9 mm. The standard deviation for these distances in the fourth session ranged from 0.7 to 6.1 mm.

### Stereotactic navigation

The results from stereotactic navigation are attached in the Supplementary Table 6. The smallest registration errors, both of 1.9 mm, were recorded in case of two registrations of the positions without pneumoperitoneum in supine position with straight legs by means of a conventional CT-scan with an identical specimen positioning.

### Discussion

This is the first study to evaluate the impact of a changing patient position as required by rectal surgery on the patient anatomy, sacral tilt, and skin fiducials position. The study provides essential anatomical and dynamic data, which may open the way for the use of current optical navigation systems in pelvic organ surgery. These data can serve as a basis for an optimal registration process in order to prevent inaccurate registration, which can render a guidance system worse than useless and even dangerous [6].

We introduce a new method to determine the change in patient anatomy, sacral tilt, and skin fiducial position using an image computing platform, hence facilitating computerized quantitative image analysis. Markers were placed manually by using a 3D Slicer software. An excellent repositioning accuracy for the repeated placement of S1-6 markers in one scan three times suggests a proper method for marker placement.

Other studies which have contributed to the knowledge of pelvic organ motion mainly include studies in radiation therapy. Multiple studies have been performed to quantify the motion of pelvic organs such as prostate, bladder, and vagina in order to optimize the planning of the volume which should be targeted by radiation to compensate for tissue deformation [7, 8]. The role of rectal distension on prostate motion had also been investigated [9].

Studies looking into prostate position demonstrated motion of the prostate as a result of motion at the level of the legs. One study investigating prostate motion reported that immobilization at the level of the patient’s legs in a supine position improves the set-up accuracy of radiotherapy as compared to an immobilization at pelvic level [7]. Other factors influencing pelvic organ motion include rectal distension. Strong evidence has shown that rectal distension on treatment planning CT-scan decreased the probability of biochemical and local control in prostate cancer patients who were treated with radiotherapy without daily image-guided prostate localization [9].

Most of these studies compared 3D organ contours between different scans [8]. This technique could be accurate provided that there is no change in organ shape and provided that there are no geometrical uncertainties. However, positional change is the subject of our investigation.

---

**Table 3** The sacral tilt was determined between the plane formed by connecting the three points S4–S5–S6 and the vertical plane. The results of all the four human anatomical specimens are depicted

| Human anatomical specimen | Sacral tilt angle (°) | Mean angle (sd) |
|---------------------------|----------------------|----------------|
| 1. Without wedge          |                      |                |
| Supine, legs straight, no pneumoperitoneum | 27.6 | 29.1 |
| 2. Without wedge          |                      |                |
| Supine, legs straight, pneumoperitoneum | 20.8 | 21.2 |
| 3. Without wedge          |                      |                |
| Supine, hip abduction 60° | 5.9 | 6.5 |
| 4. With wedge             |                      |                |
| Supine, hip abduction 60° | 17.9 | 20.1 |
| 5. Without wedge          |                      |                |
| Supine, hip abduction 60° | 23.8 | 25.1 |
| 6. With wedge             |                      |                |
| Supine, hip abduction 60° | 37.3 | 38.2 |

---

Variations. In contrast, it resulted in fewer variations for the fourth session.

**Skin fiducial position**

As expected, displacement of skin fiducials was significantly impacted by pneumoperitoneum induction, rendering it useless in the perspective of optical navigation. This observation led to the abandonment of the method in the last two experiments. The distances between S4 and each individual skin fiducial were determined for the last two human anatomical specimens and are depicted in Supplementary tables 2–5. The standard deviation for these distances in the third session ranged from 0.4 to 2.9 mm. The standard deviation for these distances in the fourth session ranged from 0.7 to 6.1 mm.

**Stereotactic navigation**

The results from stereotactic navigation are attached in the Supplementary Table 6. The smallest registration errors, both of 1.9 mm, were recorded in case of two registrations of the positions without pneumoperitoneum in supine position with straight legs by means of a conventional CT-scan with an identical specimen positioning.

**Discussion**

This is the first study to evaluate the impact of a changing patient position as required by rectal surgery on the patient anatomy, sacral tilt, and skin fiducials position. The study provides essential anatomical and dynamic data, which may open the way for the use of current optical navigation systems in pelvic organ surgery. These data can serve as a basis for an optimal registration process in order to prevent inaccurate registration, which can render a guidance system worse than useless and even dangerous [6].

We introduce a new method to determine the change in patient anatomy, sacral tilt, and skin fiducial position using an image computing platform, hence facilitating computerized quantitative image analysis. Markers were placed manually by using a 3D Slicer software. An excellent repositioning accuracy for the repeated placement of S1-6 markers in one scan three times suggests a proper method for marker placement.

Other studies which have contributed to the knowledge of pelvic organ motion mainly include studies in radiation therapy. Multiple studies have been performed to quantify the motion of pelvic organs such as prostate, bladder, and vagina in order to optimize the planning of the volume which should be targeted by radiation to compensate for tissue deformation [7, 8]. The role of rectal distension on prostate motion had also been investigated [9].

Studies looking into prostate position demonstrated motion of the prostate as a result of motion at the level of the legs. One study investigating prostate motion reported that immobilization at the level of the patient’s legs in a supine position improves the set-up accuracy of radiotherapy as compared to an immobilization at pelvic level [7]. Other factors influencing pelvic organ motion include rectal distension. Strong evidence has shown that rectal distension on treatment planning CT-scan decreased the probability of biochemical and local control in prostate cancer patients who were treated with radiotherapy without daily image-guided prostate localization [9].

Most of these studies compared 3D organ contours between different scans [8]. This technique could be accurate provided that there is no change in organ shape and provided that there are no geometrical uncertainties. However, positional change is the subject of our investigation.
and consequently, we cannot assume that there is no change. Additionally, segmentation of organ contours is more time-consuming and difficult as compared to marking certain landmarks.

The experimental protocol was tailored on the results of the first two experimental sessions. The pneumoperitoneum was abandoned as a variable in the last two human anatomical specimens since it was shown to be associated with extensive displacement of skin fiducials. The 10-degree wedge was introduced since a sacral retroversion was noted when hip flexion and/or abduction was applied in the first two sessions. Our hypothesis that the wedge decreases sacral tilt was not confirmed since a sacral retroversion was also noted with wedge use. However, interestingly, pelvic organ motion was reduced significantly, suggesting a benefit from using a wedge.

Based on our experiments, we can conclude that the following aspects should be taken into account and included in the protocol for an optimal set-up of point-merge stereotactic navigation in pelvic surgery: patient position registration should be performed without pneumoperitoneum in a similar patient position to the position during preoperative CT-scanning with fiducials. This is because a changing patient position results in skin fiducial motion hampering accurate patient position registration. A supine position with straight legs is the preferred position. The patient tracker should be fixed into the iliac bone to integrate the change in sacral tilt angle into the surgical navigation system since a change is expected to occur when switching position. Finally, a forced sacral tilt seems to minimize the change in patient anatomy.

Limitations related to stereotactic navigation include the need for maintaining a direct line of sight between the infrared camera of the navigation system and the patient and instrument tracker. This line of sight can be hampered by the legs of the patients that are placed in lithotomy and the surgeon that is positioned between the patient’s legs. Another limitation is that stereotactic navigation relies on preoperative images for accurate navigation. Therefore, real-time geometric changes in pelvic anatomy caused by for example tissue dissection and traction are known to affect the accuracy of stereotactic navigation.

Other factors which should be considered based on earlier studies on pelvic organ motion are the following: rectal and bladder volume should be equal during the scans which are used for registration/navigation, as well as intraoperatively. Consequently, the bladder should be emptied before scanning as well as intraoperatively via the placement of a catheter. The rectum should be emptied by means of an enema. In case of transanal TME, the rectum should be emptied just before closing the pure-string. The pelvic diaphragm muscle tension should be equal during the scans, as well as intraoperatively.

Future directions which can further improve the accuracy of stereotactic pelvic navigation include the use of registration methods which do not require skin fiducials and which use real-time intraoperative imaging to perform patient position registration. A patient tracker which can be fixed to the pelvis and scanned intraoperatively would eliminate the need for skin fiducials along with its associated risks of imprecision. Nowadays, intraoperative CT-scan guidance is facilitated with the use of hybrid ORs which are equipped with real-time C-arm CT-scans. However, the diameter of the current real-time C-arms CT-scan is a limiting factor since it is too small to scan a patient positioned in lithotomy. Other imaging techniques which have been reported and which are suggested to improve accuracy providing a continuous intraoperative real-time feedback include US imaging which can be fused with CT or MRI data sets [10].

Surgical navigation is likely to improve the accuracy and efficiency of rectal surgical procedures in which it is difficult or impossible to identify and dissect along the anatomical planes. In conclusion, the current study shows that accurate stereotactic surgical pelvic navigation is feasible when taking into account several aspects of registration set-up.

Acknowledgements The authors want to thank Manon Becqueart, Murad Bouhadiar, Gaël Fourné, Christian Gonzalez, Jung-Myun Kwak, Julie Mahe, and Alain Rohrfrisch for their contributions to the successful implementation of this study. We also thank Guy Temporal and Christophe Burel for their editorial assistance. The equipment used during these test was made available by Medtronic.

Compliance with ethical standards

Disclosures J. Marescaux is president of both IRCAD and IHU Strasbourg, which are partly funded by Karl Storz, Medtronic, and Siemens Healthcare though he has no direct conflict of interest with content discussed in this manuscript. A.G.F. Melani receives remuneration (payment for services not otherwise identified as salary such as consulting fees, honoraria) from Medtronic, Ethicon, Intuitive Surgical, and Verb Surgical though he has no direct conflicts of interest with content discussed in this manuscript. A.R. Wijsmuller, L.G. Romagnolo, V. Agnus, C. Giradeau, and B. Dallemagne have no conflicts of interest or financial ties to disclose.

Open Access This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made.

References

1. Mezger U, Jendrewski C, Bartels M (2013) Navigation in surgery. Langenbecks Arch Surg 398(4):501–514
2. Wadley J et al (1999) Pre-operative planning and intra-operative guidance in modern neurosurgery: a review of 300 cases. Ann R Coll Surg Engl 81(4):217–225
3. Atallah S, Martin-Perez B, Larach S (2015) Image-guided real-time navigation for transanal total mesorectal excision: a pilot study. Tech Coloproctol 19(11):679–684
4. Atallah S, Nassif G, Larach S (2015) Stereotactic navigation for TAMIS-TME: opening the gateway to frameless, image-guided abdominal and pelvic surgery. Surg Endosc 29(1):207–211
5. Fedorov A et al (2012) 3D Slicer as an image computing platform for the quantitative imaging network. Magn Reson Imaging 30(9):1323–1341
6. Fitzpatrick JM (2010) The role of registration in accurate surgical guidance. Proc Inst Mech Eng H 224(5):607–622
7. Fiorino C et al (1998) Set-up error in supine-positioned patients immobilized with two different modalities during conformal radiotherapy of prostate cancer. Radiother Oncol 49(2):133–141
8. van Herk M et al (1995) Quantification of organ motion during conformal radiotherapy of the prostate by three dimensional image registration. Int J Radiat Oncol Biol Phys 33(5):1311–1320
9. de Crevoisier R et al (2005) Increased risk of biochemical and local failure in patients with distended rectum on the planning CT for prostate cancer radiotherapy. Int J Radiat Oncol Biol Phys 62(4):965–973
10. Prada F et al (2014) Fusion imaging for intra-operative ultrasound-based navigation in neurosurgery. J Ultrasound 17(3):243–251