Energy Transfer Between Rare Earth-doped Ceramic Nanoparticles for Gauging Strain and Temperature in Elastic Polymers

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The field of self-reporting materials is gaining increased attention recently. These materials can convey the forces applied to them without the need to integrate external devices. The ability to report strain exerted onto polymers is especially important, as it might give indication of high levels of force that may damage the material. These materials could also be applied to in-dwelling medical devices such as artificial tendons and heart valves. In this work, we designed a self-reporting system based on energy transfer (ET) between rare earth-doped ceramic nanoparticles (RED-CNPs). When external strain and heat are applied, the efficiency of the ET changes, resulting in changes in the emission spectra. We chose particles that are excited by 808 nm radiation and emit in the over-thousand-nanometer near infrared, since this range offers high penetration to biological tissues. Nanoparticles (NPs) were synthesized using the thermal decomposition method and then extensively characterized. X-ray diffraction analysis revealed that the doped NaYF₄ crystals are in the β-phase, while inductively coupled plasma emission spectrometry demonstrated the existence of two types of NPs: NaYF₄: Nd³⁺, Yb³⁺ and NaYF₄: Er³⁺. The absorption and emission of the particles showed no ET between the two kinds of NPs when simply mixed together. In order to reduce the interparticle distance and allow ET, RED-CNPs were coated with polydopamine (PDA) and then conjugated with a polymeric linker. Scanning electron microscopy, dynamic light scattering and absorption analysis showed the successful coating with PDA and the creation of interconnected NP networks. Emission from the conjugated system showed evidence of ET, while changes in the emission lifetime of Yb as measured by time-gated imaging further suggested ET between Yb and Er. Finally, the conjugated system was integrated into poly(dimethylsiloxane) and it was shown that as strain or heat are exerted onto it, the emission spectra under 808 nm excitation is varied.

Keywords: NIR, Energy Transfer, Self-reporting materials, RED-CNP

1. Introduction

The ability to monitor strain in various materials is of great importance. Over the past decades, a variety of methods to detect strain have been developed, including mechanical, electrical and optical ones [1]. For example, the integration of flexible fiber optic sensors into polymers is used in biomedical applications where qualities of light
travelling in the fiber, such as intensity, phase and wavelength, are modified in response to forces applied to the polymer [2]. The disadvantage of these techniques is that they require incorporation of physical components into the polymer, which could vary the material’s physical properties. However, new approaches for strain-evaluation that involve incorporation of luminescent agents into the polymer are being developed. By observing the changes in parameters such as luminescent intensity, lifetime and wavelength, it is possible to assess the strain that is applied to the host material. Some examples of these mechanochromatic systems include the use of aggregates of dye molecules that change their emission wavelength when mechanical force separates the aggregates into monomers. Rossi et al. conjugated pyrene molecules to poly(hydromethylsiloxane) and integrated them into a poly(dimethylsiloxane) (PDMS) elastomer [3]. Upon stretching, a decrease in the aggregate/monomer intensity ratio was detected. Another approach that might be employed to assess strain is by using Förster resonance energy transfer (FRET). This optical phenomenon occurs when an excited fluorophore ("donor") transfers its energy to an adjacent fluorophore ("acceptor"), which can then be emitted as a photon of a longer wavelength [4]. This energy transfer (ET) is non-radiative and occurs through dipole-dipole coupling, meaning its efficiency is proportional to the inverse of the sixth power of the distance between the two molecules. Radiative ET may also occur when distances are larger than a few nm and the efficiency in that case is inversely proportional to the second power of the distance. For example, Karthikeyan and Sijbesma have used FRET to detect strain in thermoplastic elastomers [5]. They conjugated donor and acceptor molecules to a polymer that was incorporated into the elastomer. In resting state, the fluorophores were sufficiently close to each other and upon excitation, emission from both species was detected. However, when the polymer was stretched, the distance between the fluorophores increased and an increase in the donor/acceptor emission was detected. We have recently used a much simpler methodology to report strain by ET and incorporated fluorescein and rhodamine B into PDMS by simple mixing and curing [6]. Moreover, we were able to create a 2-dimensional strain map by using a simple digital camera and image processing software.

When designing optical materials for use in indwelling medical devices, one has to take into account the absorption and scattering of body tissues. While the current generation of mechanochromatic systems uses almost exclusively visible light, this range of electromagnetic radiation has very low penetration of living organisms [7]. On the other hand, near infrared (NIR) light has a much higher penetration of biological tissues and is recently gaining increased attention for use in bio-imaging [8,9]. However, while organic dyes are the major NIR agents used for bioimaging, they suffer from several limitations such as rapid photodegradation and short luminescence lifetime [10]. One of the promising NIR agents currently tested for various bio-applications is rare earth doped ceramic nanophosphors (RED-CNPs). These are ceramic nanocrystals such as NaYF₄ and LaPO₄ that are doped with lanthanide ions such as Er³⁺, Yb³⁺, Nd³⁺, Tm³⁺, etc. These NIR agents offer high stability, emission in various wavelengths and luminescence lifetime in the order of milliseconds [11]. Recently, Van de Haar et al. have demonstrated intraparticle FRET (IFRET) between LaPO₄ NPs that were doped with either Tb or Eu [12]. When the two types of particles were 3 nm or less from each other, ET from Tb to Eu occurred, resulting in emission at 700 nm.

In this work, we set out to use a system comprised of two types of RED-CNPs that can maintain ET that is affected by various stimuli, including strain and heat. Similar to our previous work, when the distance between donor and acceptor NP is small enough, ET is efficient [6]. However, when stretched this distance increases thus decreasing the ET efficiency and changing the emission spectrum. To keep the interparticle distance small enough to allow efficient ET, we first coated them with polydopamine (PDA) and then used this coating to conjugate the particles to a poly(ethylenimine) (PEI) linker (Scheme 1). PDA is a biomimetic polymer based on mussel adhesive protein used by these organisms to adhere to surfaces [13]. It was discovered that PDA can coat almost any surface or particle and this coating can later interact with molecules or other materials via covalent or non-covalent interactions. This ability to functionalize surfaces has been used extensively to endow different properties to these materials, such as antibacterial, antifouling and anti-cancer activity [14–16]. In the case of covalent bond-forming, PDA is reactive towards amine groups which are present in PEI. After particle conjugation, they were integrated into biocompatible PDMS and the ability of the system to respond to strain and heat was evaluated.
2. Experimental

2.1. Materials

All materials were purchased from Wako Chemicals (Japan) unless stated otherwise. Oleic acid (OA), yttrium chloride hexahydrate (YCl₃·6H₂O), dopamine (DA) and nitrosyl tetrafluoroborate (NOBF₄) were purchased from Sigma-Aldrich (MO, USA).

2.2. RED-CNP synthesis

NPs were synthesized according to the thermal decomposition method [8]. Shortly, 30 mL 1-octadecene (ODE) and 12 mL OA were placed in a 3-necked flask with aqueous solutions of the different lanthanide chlorides. The quantities of the metals depended on the intended composition of each NP, but in all cases the combined amounts added up to 1 mmol. The flask was heated while being stirred and pumped with N₂. Then 10 mL of NaOH and NH₄F (2.5 and 4 mmol, respectively) in methanol (MeOH) was added and the mixture was heated to 300 °C. Particles were then wash-centrifuged (10 min, 30,000 rpm; 3-30 ks, Sigma, Germany) and suspended in hexane.

For PDA coating and PEI conjugation, particles were first stripped of their OA chelation and replaced with BF₄⁻. NPs in hexane (5 mg/mL) were mixed with NOBF₄ (10 mg/mL in DMF) overnight. After washing, the particles were suspended in water and reacted with dopamine (DA, 0.05 mg/mL) in 40 mL Tris buffer (pH 8.5, 0.1 M) for 1 h to yield M@PDA particles. Particles were then washed in water and ethanol (EtOH). Particles were then suspended in 25 mL Tris buffer (pH 9.5, 0.1M) and reacted with 100 µL PEI (branched, MW=1800) with overnight stirring at 40 °C. Incorporation in PDMS was done by suspending the particles in 0.5 mL EtOH with TiO₂ (0.01% w/w), followed by mixture in the oligomer and crosslinker (1:0.1 mL). The mixture was then degassed and cured at 65 °C overnight to yield strips of 30×10×1 (L×W×H) mm.

2.3. Physical and optical characterization

Samples were characterized by X-ray diffraction (XRD) using CuKα radiation (RINT-TTR III, RIGAKU, Japan). The crystallite size \( D \) of the particles was evaluated using the Scherrer equation (Eq. 1), where \( K \) is the shape factor (≈0.9), \( \lambda \) is the X-ray wavelength (0.154), \( \beta \) is the full width at half maximum (FWHM) and \( \theta \) is Bragg's angle. [16]:

\[
D = \frac{K\lambda}{\beta \cos \theta}
\]
The peak chosen was at 43° (201).

The morphology and size distribution were observed via scanning electron microscopy (SEM; HD-4200, Hitachi, Japan). The hydrodynamic diameter of the NPs was measured by a dynamic light scattering (DLS) analyzer (LB-550, Horiba, Japan).

Metal content was evaluated using inductively coupled plasma (ICP) emission spectrometry (ICPE-9000, Shimadzu Co., Kyoto, Japan). Samples were first digested in aqua regia (HCl/HNO₃, 3:1) overnight under stirring and then diluted in doubly distilled water (DDW). Quantification was done against multi-element calibration aqueous solutions: Ce, Dy, Er, Eu, Gd, Ho, La, Lu, Nd, Pr, Sc, Sm, Tb, Th, Tm, Y, Yb (Perkin Elmer, CT, USA).

Absorption was measured with a V-770 spectrometer (Jasco, Japan). NIR Fluorescence was measured with Avantes spectrometer (NIR-256-1.7, Netherlands). Irradiation was done with 808 nm (normally at 1.5 W/cm²) fiber-coupled laser diode (FL-FCSE08-7-808, Focus Light, China).

2.4. Time-gated imaging and lifetime measurement

The fluorescence lifetime was analyzed by time-gated imaging (TGI) system, which is composed of pulsed laser and an NIR camera (ARTCAM-0016TNIR; Artlay Co. Ltd., Tokyo, Japan) synchronized by a pulse generator (DG535; SRS Inc., Sunnyvale, CA, USA). A pulsed laser diode (wavelength: 808 nm; power: 0.7 W/cm²) was used to generate 1 ms pulses at a repetition rate of 20 Hz. The pulse-to-pulse separation was set to 49 ms, during which the fluorescence of the phosphors disappears completely. Two 850-nm long-pass filters (86-452; Edmund Optics, NJ, USA) were placed in front of the NIR camera. To obtain the fluorescence decay curves, a series of fluorescence images (8-bit) was acquired at delayed times (t_delay) triggered by the pulse generator, where t_delay ranged from 0 to 900 μs in increments of 100 μs.

2.5. Strain and temperature measurements

PDMS-integrated samples were gradually stretched and irradiated with 808 nm laser (2 W/cm²). Their emission spectra were measured with an NIR spectrometer. Similarly, PDMS strips were heated with a hot air gun and their spectra analyzed under 808 laser irradiation (2 W/cm²).

3. Results and discussion

3.1. Particle synthesis and characterization

Three types of OA-chelated RED-CNPs were synthesized: NaYF₄: Nd₃¹%, Yb₃¹% (Nd/Yb@OA), NaYF₄: Er₃% (Er@OA) and NaYF₄: Nd₃¹%, Yb₃¹%, Er₃% (Nd/Yb/Er@OA) according to the thermal decomposition method [8]. The composition of Nd/Yb@OA was designed according to the one used by Chihara et al., which ensures very bright emission from Yb [18]. In the aforementioned crystal lattice, 808 nm radiation is absorbed by Nd’s ⁴F₅/₂ energy level, followed by relaxation to ⁴F₃/₂, from which energy is transferred to the ²F₅/₂ level of Yb (energy level diagram is shown in Fig. S1) [19]. We optimized the Er content in Er@OA for maximum emission (Fig. S2), so that energy could be transferred from Yb to Er (²F₅/₂ → ⁴I₁₁/₂), followed by emission at around 1500 nm. By comparing the Yb emission at 1100 nm to that of Er at 1500 nm we intend to infer the distance between the two particles. After washing and purification, NPs were suspended in hexane for physical characterization. First, the size of both particles was assessed using DLS and was found to be around 45 nm in diameter (Nd/Yb@OA=43.0 ±9.9 nm, Er@OA=46.7 ±9.5 nm, Fig. 1A). Then particles were deposited on Si wafers for SEM analysis. As seen in Figure 1B, particles were fairly uniform in size and their average size was 43.5 nm. XRD analysis was carried out on dry powders of the particles and demonstrated the crystals are in β-phase (reference pattern: JCPDS 16-0334, Fig. 2). The crystalline size was found to be about 11.5 nm in both cases. Particles were also analyzed for their metal content by ICP and their lanthanide composition was found to be almost identical to the theoretical one (Table S1).

The absorption spectra of the NPs are given in Fig. 3A, and for Nd/Yb@OA many sharp absorption peaks can be seen, most of which are attributed to Nd. Most notable are the peaks at around 800 nm
Fig. 2. XRD patterns for dried RED-CNPs.

\(^{1}I_{9/2} \rightarrow ^{4}F_{5/2}, \ 2H_{9/2}\) and 600 nm \(^{4}I_{9/2} \rightarrow ^{4}G_{5/2},\ 2G_{7/2}\). The absorption spectrum of Er@OA has far fewer sharp peaks, with a small one around 1000 nm \(^{4}I_{15/2} \rightarrow ^{4}I_{11/2}\) [8]. Next, the emission of the particles suspended in hexane was determined and is shown in Fig. 3B. The emission at around 1100 nm is a combination of transitions \(^{4}F_{3/2} \rightarrow ^{4}I_{11/2}\) and \(^{2}F_{5/2} \rightarrow ^{2}F_{7/2}\) from Nd\(^{3+}\) and Yb\(^{3+}\), respectively (Fig. S1) [20]. The peak at around 1300 nm corresponds to the transition \(^{4}F_{3/2} \rightarrow ^{4}I_{13/2}\) from Nd\(^{3+}\). The emission of Er@OA presents one broad peak at around 1500 nm, which is attributed to the \(^{4}I_{13/2} \rightarrow ^{4}I_{15/2}\). This demonstrates the fact that Er can be weakly excited by 808 nm irradiation. Irradiation of a 1:1 mix of the two solutions showed no relative change in any of the peaks. If ET were to occur between Yb to Er, one would expect an increase in the Er peak and a decrease of the Yb one (1500 and 1100 nm, respectively). Another good indication of ET would be a decrease in the 1100/1300 nm peak ratio. While the emission from Yb should be reduced due to ET to Er, the Nd peak should not be affected. To confirm this hypothesis, particles containing all three elements (Nd/Yb/Er@OA) were prepared and their emission profile was compared to that of Nd/Yb@OA. Indeed, while the 1100/1300 nm peak ratio of Nd/Yb@OA was 1.2, co-doping the NPs with Er reduces the ratio to 0.6 (Fig. S3). However, in the case of a mixture of Nd/Yb@OA and Er@OA, that ratio remains unchanged. This demonstrates the fact that in a typical solution the distances between the two types of particles are too large for ET to occur.

3.2. Particle conjugation

In order to decrease the interparticle distance, we set out to conjugate NPs with a polymeric linker. This was done by first coating each type of NP with a PDA shell, which is reactive towards amine functional groups [13]. This reactivity can later be used in order to conjugate it with a PEI linker, thus creating a network of interconnected RED-CNPs. PDA coating was done according to the method used by Liu et al. [21]. Shortly, each type of NP in hexane was mixed with a solution of NOBF\(_4\) in DMF overnight to yield particles chelated by BF\(_4^-\) (M@BF\(_4^-\)). Particles were then separately suspended in a DA solution in Tris buffer (pH 8.5) for 1 h to yield PDA-coated RED-CNPs (M@PDA). First, DLS analysis was done on particles coated with PDA (Fig. 4A). While NPs chelated by OA were about 45 nm in size, the coated particles increased in size to about 50 nm, indicating a shell of 2.5 nm thickness. In the procedure reported by Liu et al. a similar size was achieved, as measured by transmission electron microscopy (TEM). It should be noted that the difference in size herein was measured by DLS, which measures the hydrodynamic radius. For a hydrophilic polymer such as PDA, it is possible that a layer of water
around the polymer increases the measured size, while the actual size and shell thickness might be smaller. The absorption spectrum of coated NPs is given in Fig. 4B and the characteristic broad absorption spectrum of PDA can clearly be seen [13]. While most of the Nd and Yb peaks are covered by PDA’s absorption, some peaks can still be seen, most notably around 600 and 800 nm.

After confirmation of PDA coating, the two types of particles were reacted with PEI in Tris buffer (pH 9.5) overnight to give conjugated Nd/Yb@PDA-PEI-Er@PDA. Examination of the DLS results in Fig. 4A show the reacted particles increased in size significantly. From 50 nm, the average size grew to about 800 nm. This is likely due to formation of big clusters of particles that are bound together by PEI. Further proof of this notion is given by SEM images shown in Fig. 5. Simply mixing the 2 types of PDA-coated NPs gives large plaques of material which are composed of NPs and PDA aggregates. The plaques are usually more than 10 µm in size, although smaller clusters also appear. The PDA and RED-CNPs parts can easily be distinguished by the different contrast. The polymeric parts are made of particles of about 50 nm, which is typical for PDA (Fig. S4) [22]. The RED-CNPs are clustered together tightly, however their size is difficult to assess due to the merging of the PDA shells. Nd/Yb@PDA-PEI-Er@PDA present a drastically different shape, characterized by round clusters of several hundreds of nm. The particles are less packed together, probably due to the PEI spacer. A polymeric shell can clearly be seen around the RED-CNPs, however no large PDA plaques are attached to the clusters. This difference in morphology between particles reacted with and without PEI demonstrates the successful covalent conjugation of the linker. Additional SEM images are given in Fig. S4.

The PDA-coated particles were then dispersed in water and their emission spectra was evaluated under irradiation at 808 nm. As seen in Fig. 6A, all particles lose some of their emission compared to their OA-chelated form, possibly because of PDA absorption or quenching by water. When comparing the separate PDA-coated particles to their PEI-conjugated form, two differences are apparent. Firstly, for Er@PDA the emission at 1500 nm is very low, mostly because of Er’s low absorption at 808 nm. However, upon conjugation to Nd/Yb@PDA, this emission quadruples, giving a Yb/Er emission ratio of 5. This is a big reduction from the ratio calculated for the emissions from separate Nd/Yb@PDA and Er@PDA, which is 30. It should be noted that this increase cannot be attributed to reabsorption of emission from Yb and Nd, since Er is not excited by radiation in 1100 and 1300 nm. Secondly, the Yb/Nd emission ratio for Nd/Yb@PDA is reduced from 1.6 to 1.1, in the conjugated form. This is not a dramatic decrease such as in the case of Nd/Yb/Er@OA, but in the latter case the distance between the lanthanides is much smaller, which allows for a far more efficient ET. These two features of the water dispersed Nd/Yb@PDA-PEI-Er@PDA demonstrate that interparticle ET probably occurs between Yb and Er.

Another evidence of ET between Yb and Er can be obtained by observing change in the emission lifetime of Yb with or without Er [19]. To that end, samples were dried on glass slides,
irradiated with 808 nm pulse laser and their emissions analyzed with an NIR camera. First, the lifetime of Yb in Nd/Yb@OA was compared to that of Nd/Yb@OA and Nd/Yb@PDA-PEI@PDA (p > 0.05), N=3.

Nd/Yb@PDA-PEI-Er@PDA, again a non-linear pattern emerges. Between 0 and 300 µs the lifetime is 290 µs, which is very similar to the same period measured for Nd/Yb@OA. The rest of the decay is characterized by a very long lifetime, of about 920 µs. This slow decay might be due to the chelation of Er by PDA, which stabilizes the excited state and slows the emission from the system. The decay rate in the periods of 0-300 µs is given in Fig. 6B and it can be seen that while it is very similar for particles with Er, it is significantly longer for Nd/Yb@OA alone. This is a potent demonstration that interparticle ET in Nd/Yb@PDA-PEI-Er@PDA reduces the lifetime of Yb, in a way similar to that of intraparticle ET in the Nd/Yb/Er system.

3.3. Strain and temperature monitoring in PDMS

Finally, the ability of the conjugated RED-CNPs system to serve as a sensor for various stimuli was tested. Nd/Yb@PDA-PEI-Er@PDA were incorporated into the biocompatible elastic polymer PDMS and the change in ET between Yb and Er as a function of applied strain was evaluated. It is hypothesized that any strain applied to the conjugated system would result in an increase in the distance between Nd/Yb@PDA and Er@PDA, which would translate to a decrease in the ET efficiency. This change in efficiency could be detected by monitoring the emission ratio between Yb and Er.

To verify this hypothesis, strips of PDMS impregnated with Nd/Yb@PDA-PEI-Er@PDA were gradually stretched under illumination with 808 nm laser while their emission spectra were recorded. Figure 7A shows the change in Yb/Er emission ratio as strain is applied to the PDMS strip. While all of the emission peaks are reduced due to stretching and the practical dilution of the system, the response of each element is different. Whereas the change in emissions at 30% strain from Nd and Er are -40% and -50%, respectively, the change in Yb emission is only -25%. Indeed, it can be seen that as the elastomer is stretched, the emission of Yb increases compared to that of Er, indicating a reduction in ET efficiency. From a ratio of about 1 in the relaxed state, the ratio increases by 33% in the stretched state, giving a sensitivity of about 0.1 per 10% strain. This increase in the emission of Yb compared to Er demonstrates the potential use of the Nd/Yb/Er system for strain monitoring. It was also observed that the Yb/Nd ratio increased in a similar manner. It should be noted that the current system is not reusable and its response is not reversible. This
might be due to corruption of the Nd/Yb@PDA-PEI-Er@PDA aggregates under strain, possibly because they are not flexible enough. In the current study branched PEI polymers of relatively low MW (1800) were used, which might lead to highly crosslinked clusters that are rigid and are prone to breakage. For that reason, optimization of the system is still needed.

Another possible use of this system is for temperature measurement, as the effect of heat on ET between Yb and Nd has already been reported [17]. In that work it was shown that as samples containing NaYF₄: Nd³⁺, Yb³⁺ are heated, the luminescence lifetime of Yb is reduced due to phonon-assisted back transfer to Nd. It stands to reason that if the lifetime and excitation energy of Yb are reduced, the ET between it and Er will be decreased, resulting in an increase of the Yb/Er emission ratio. To test this assumption, PDMS samples with Nd/Yb@PDA-PEI-Er@PDA were heated and their emission spectra were recorded under 808 nm excitation. As seen in Fig. 7B, as temperatures increased, the ratio between the emission of Yb and Er was raised. As seen in Fig. S6, after an increase of 45 °C, the Nd peak increases by 60%, while that of Er decreases by 25%. This is consistent with energy back transfer from Yb to Nd, which reduces the available energy for ET to Er. It’s important to note the different behavior of Nd emission in the cases of either strain or heat application. While simply increasing the distance between NPs only raises the relative energy of Yb without any effect on Nd, when heat is applied the effect is on both Yb and Nd due to phonon assistance. Overall, the linear change in Yb/Er emission as the temperature increases shows that the current system might be suitable for deep tissue temperature monitoring, as NIR light can travel through several centimeters of biological tissues. This system may also be suitable for temperature sensing using TGI or emission lifetime, as those methods offer excellent sensitivity and are less affected by physiological conditions.

4. Conclusion

In this work we demonstrated the use of interparticle ET measurement as a means to gauge the strain and heat applied to elastomers. We have used two types of RED-CNPs: NaYF₄ doped with Nd³⁺ and Yb³⁺ or with Er³⁺ due to their good absorption and emission in the NIR range. This range has high penetrability to biological tissues, which might enable the use of the system in indwelling biomedical devices. We showed that simply mixing the two particles does not produce efficient ET, as evident by very low emission from Er. However, as the particles are coated with a reactive PDA shell and conjugated together with a PEI linker, the interparticle distance decreases sufficiently. This allows for ET which is evident by a decrease in the emission from Yb, accompanied by an increase from Er. Furthermore, luminescence lifetime measurements done with TGI revealed that the presence of Er in the system affects the emission from Yb. Most importantly, attaching Er-containing NPs to Nd/Yb-containing NPs shortened the luminescence lifetime of Yb in a manner resembling that of NPs containing all three elements. Finally, we evaluated the ability of our system to serve as a sensor for various stimuli. After incorporation in PDMS, we demonstrated that strain or heat applied to the polymer changes the emission profile of the system. This shows the potential use of the current setup as a self-reporting material for various uses in the medical field.

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