The Effect of Surface Electrical Stimulation on Swallowing in Dysphagic Parkinson Patients

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Abstract Surface electrical stimulation has been applied on a large scale to treat oropharyngeal dysphagia. Patients suffering from oropharyngeal dysphagia in the presence of Parkinson’s disease have been treated with surface electrical stimulation. Because of controversial reports on this treatment, a pilot study was set up. This study describes the effects of a single session of surface electrical stimulation using different electrode positions in ten patients with idiopathic Parkinson’s disease (median Hoehn and Yahr score: II) and oropharyngeal dysphagia compared to ten age- and gender-matched healthy control subjects during videofluoroscopy of swallowing. Three different electrode positions were applied in random order per subject. For each electrode position, the electrical current was respectively turned “on” and “off” in random order. Temporal, spatial, and visuoperceptual variables were scored by experienced raters who were blinded to the group, electrode position, and status (on/off) of the electrical current. Interrater and interrater reliabilities were calculated. Only a few significant effects of a single session of surface electrical stimulation using different electrode positions in dysphagic Parkinson patients could be observed in this study. Furthermore, significant results for temporal and spatial variables were found regardless of the status of the electrical current in both groups suggesting placebo effects. Following adjustment for electrical current status as well as electrode positions (both not significant, \( P > 0.05 \)) in the statistical model, significant group differences between Parkinson patients and healthy control subjects emerged. Further studies are necessary to evaluate the potential therapeutic effect and mechanism of electrical stimulation in dysphagic patients with Parkinson’s disease.

Keywords Dysphagia · Deglutition disorders · Parkinson’s disease · Electrical stimulation · Deglutition

The number of reports on the effects of therapies for dysphagia in Parkinson’s disease is still small. Reviewing the literature, positive group tendencies may be observed, although no general conclusions can be drawn from these reports [1]. Surface electrical stimulation in dysphagic Parkinson patients has not been investigated in scientific studies before. Carnaby-Mann and Crary [2] describe a small but significant summary effect size for transcutaneous neuromuscular electrical stimulation (NMES) for dysphagia in a meta-analysis. The immediate effect of surface electrical stimulation on hyolaryngeal movement in normal individuals during swallowing is described by Humbert et al. [3], who observed a reduced hyolaryngeal elevation during electrical stimulation. They hypothesized...
a higher risk of further decreased hyolaryngeal elevation during electrical stimulation in dysphagic patients who are already suffering from reduced hyolaryngeal elevation. Ludlow et al. [4] observed that aspiration and pooling are significantly reduced in chronically dysphagic patients during surface electrical stimulation with low sensory threshold levels of stimulation. Almost all subjects showed depression of the hyoid bone during motor-level stimulation at rest. However, at the maximum motor level of stimulation during swallowing, no group change in aspiration at rest. Ludlow et al. [4] observed that aspiration and pooling are significantly reduced in chronically dysphagic patients during electrical stimulation in dysphagic patients who are already suffering from reduced hyolaryngeal elevation. The application of surface electrical stimulation in dysphagic patients with Parkinson’s disease without existing evidence of therapy effects in the literature has been the rationale for this present study. This study was performed to determine the immediate effect of a single session of surface electrical stimulation using different electrode positions and electrical current states in patients with Parkinson’s disease and oropharyngeal dysphagia compared to the same protocol in a group of age- and gender-matched healthy control subjects during a videofluoroscopic swallowing study. The maximum tolerated motor level of stimulation was applied to all subjects during each swallowing act.

Methods

Patients and Healthy Control Subjects

Patients with a diagnosis of idiopathic Parkinson’s disease and dysphagic complaints were recruited from several neurological departments from diverse hospitals all over the Netherlands. The dysphagic complaints ranged from mild to severe, including slow eating due to a reduced rate of spontaneous swallowing and to rigidity, hypokinesia, and bradykinesia of the masticatory, oral, or pharyngeal musculature involved in swallowing; oral or pharyngeal passage disorder; choking on food; and coughing while drinking or eating. The patients continued using their unaltered type and dose of antiparkinsonian medication for at least 2 months and their disease was stable at the time of inclusion. The Hoehn and Yahr (H&Y) disability score was used as a clinical rating scale to assess the severity of the Parkinson’s disease (Table 1) [6]. For each patient, an age- and gender-matched control was recruited. The following exclusion criteria were used for the patients as well as for the healthy control subjects: the presence of any other neurological disease; inability to perform a swallow; deep brain stimulation (DBS); a Mini-Mental State Examination (MMSE) score below 23; severe dyskinesia of head and neck (resulting in problems with VFS recording); mental depression; head and neck cancer; severe cardiopulmonary diseases; speech therapy during the past 6 months; and surgery on the swallowing mechanism or the central nervous system. Written informed consent was obtained from all patients and healthy control subjects. This study protocol was approved by the medical ethical committee of the university medical center.

| Table 1 | Demographics of dysphagic patients with Parkinson’s disease and of healthy control subjects |
|---------|----------------------------------------------------------------------------------------------------------------------------------|
| No. of matched pair of subjects | Sex | Electrode positions | Parkinson’s disease patients | Healthy controls |
| H&Y scale | Age (years) | Age (years) |
| 1 | M | I-II-III | I | 70 | 68 |
| 2 | F | III-I-II | II | 64 | 63 |
| 3 | M | II-I-III | II | 50 | 46 |
| 4 | M | III-II-I | III | 80 | 81 |
| 5 | F | III-I-II | II | 73 | 74 |
| 6 | M | II-I-III | III | 57 | 53 |
| 7 | F | III-II-I | III | 62 | 60 |
| 8 | M | I-II-III | II | 70 | 67 |
| 9 | M | III-I-II | III | 70 | 70 |
| 10 | M | II-I-III | I | 66 | 68 |

*H&Y scale = Hoehn and Yahr scale: the range of scores is I–V, where I indicates unilateral involvement, usually with minimal or no functional disability, and a V indicates confinement to bed or wheelchair unless aided [6].
hanging skin, a skin lift was performed using medical tape to restore the contact between the skin and the muscle layer. Position I represented two electrodes horizontally above the hyoid bone (submental region). Position II represented two electrodes horizontally below the hyoid bone. Position III was a combination of positions I and II with four electrodes connected on each side of the midline of the neck (Fig. 1).

For each electrode position, the status of the electrical current was three times “on” and once “off,” in random order. The VitalStim stimulator cycles automatically off for 1 s every minute. It was ensured that the swallow on VFS with the electrical current turned “on” did not occur during this 1 s “off” period. The maximum tolerated stimulation level resulting in maximum muscle contraction without spasm was applied in accordance with Ludlow et al. [4]. The stimulation intensity was raised gradually in steps of 0.5 mA until the “grabbing sensation” or maximum tolerated stimulation threshold was reached. Before each swallow, the threshold was reconfirmed to correct for fatigue of the muscles. For this purpose, the stimulation intensity was raised gradually as described before. Each patient and his or her corresponding matched healthy control subject underwent the exact same protocol of electrode positions and electrical current states.

Swallowing Assessment

Prior to the experiment, all subjects had a clinical examination by a laryngologist and a speech and language pathologist. The single-session protocol of electrical stimulation was performed during a standardized videofluoroscopic swallowing protocol of 12 trials with thin liquid. Each trial contained 10 cc of low-density barium (40% w/v) delivered orally by a syringe. The subjects had to swallow the bolus after it had been accurately delivered by a syringe in the oral cavity resulting in a motor challenge without any preparatory cue. During the VFS, subjects were seated upright in lateral position wearing their dental prosthesis if present. The field of the videofluoroscopic image included the lips, oral cavity, cervical spine, and proximal cervical esophagus. A coin of 5 Euro cents was affixed to the retroauricular skin as a reference distance to correct for magnification (calibration). Videofluoroscopic images were obtained with a Philips Diagnost 97 system (Philips Medical Systems, Eindhoven, the Netherlands) and recorded on cassette at 25 frames per second using a mini-DV camcorder Panasonic AG-DVC30 (Matsushita Electric Industrial Co., Osaka, Japan). Sounds were recorded simultaneously. In the event of mild aspiration during a trial, the examination was continued. If severe aspiration was observed, the examination was ended. All VFS examinations were performed within 90–120 min after the intake of antiparkinsonian medication. During this period called the “on” motor phase, the levodopa motor effect is maximal [8].

Selection of Variables

For quantitative assessment of the swallow, specialized software was used (Image & Physiology SL, Barcelona, Spain) to capture, digitize, and measure all swallowing sequences [9]. The capture rate was 25 frames per second. Timed variables were determined for the biomechanical analysis of swallowing [10]. The pharyngeal inlets and outlets were identified frame by frame by both raters during each pharyngeal swallow: moment of opening and closing of the glossopalatal junction (GPJ); moment of opening and closing of the velopharyngeal junction (VPJ); moment of opening and closing of the laryngeal vestibule (LV); and moment of opening and closing of the upper esophageal sphincter (UES). Using definitions of penetration and aspiration according to Rosenbek et al. [11], the frame exhibiting penetration or aspiration was marked as a timed event.
Movement patterns of the hyoid bone were used as spatial variables to analyze the swallowing function quantitatively [12]. For each swallow, three reference points were marked in each video frame: the anterior/superior corner of the hyoid bone and the anterior/inferior corner of the third and fifth cervical vertebral bodies. The y axis was defined by the anterior/inferior corner of the third and fifth cervical vertebral bodies. Perpendicular to the y axis, the x axis crosses at the anterior/inferior corner of the third vertebral body. By marking these reference points in each frame, movements of the subject in any plane could be corrected (Fig. 2). Next, the extent of movement of the hyoid bone in the x-y coordinate system over time was analyzed by means of specialized software.

Furthermore, visuoperceptual variables were scored for each VFS swallow. The variables are as follows: preswallow anterior and preswallow posterior spill, lingual pumping, swallow hesitancy, piecemeal deglutition, delayed initiation of the pharyngeal reflex, postswallow oral residue, postswallow vallecular pooling, postswallow pyriform sinus pooling, and the penetration aspiration scale of Rosenbek et al. [11, 13, 14]. In this 8-point scale (1–8), lower scores refer to normal functioning and higher scores refer to more severe disability. Following consensus training, two experts assessed each swallow independently at varying speed, ranging from normal to slow motion to frame-by-frame viewing. The consensus training in visuoperceptual evaluation was accompanied by a manual, including strict, well-defined guidelines to rate these ordinal variables. The exact interpretation per level of each of the three- or five-point scales was trained during five separate sessions with intervals of 1 week. During these intervals the expert raters had to accomplish test trials separately that were discussed during the next session.

Previous research by Baijens et al. [15] has described the reliability or intra- and interrater agreement on several quantitative and qualitative parameters in VFS. Only parameters that proved to be sufficiently reliable have been included in the present study (Table 2). All measurements and ratings were performed independently by two experienced judges. Both judges were blinded to the group, electrode position, and status of the electrical current (on/off). To optimize blinding to the electrode position during VFS, four electrodes were placed on the skin according to the electrode positions mentioned above. Although the cables were connected to all four electrodes, only the electrodes of the position being studied during a specific swallowing act were stimulated (Fig. 2). The trials of all subjects were scored in randomized order. Before interpreting the study outcome, the intrarater and interrater reliabilities were determined. To obtain the intrarater reliability, each rater performed repeated measurements of all temporal, spatial, and visuoperceptual variables during the second swallow of each electrode position for all subjects (patients and healthy control subjects) within a period of 2 weeks.

Statistical Analysis

All temporal and spatial variables had six technical replications for each subject, as these were repeatedly measured in three different electrode positions (suprahyoidal, infrahyoidal, and bilateral combination) during two electrical current states (on/off), whereas the visuoperceptual variables had 12 technical measurements for each subject. Variables were measured for all electrode positions and electrical current states in both healthy control subjects and Parkinson’s patients (Table 1). Random intercept models were fit for all reliable VFS outcome parameters. This was done twice: for the patients’ only and for all subjects. In the former case, the objective was to determine whether the electrode positions and/or the status of the electrical current affected the VFS outcomes of Parkinson’s patients. Patients were defined as random effects, whereas electrode positions and status of the electrical current were defined as fixed effects. This model accounts for the correlation induced by the nesting of repeated measurements within subjects. The alternative analyses, using all subjects, aimed at testing additionally for group differences, while concurrently adjusting for electrode position and electrical current status. However, for all subjects the random effect was no longer a single subject but a pair, composed of one patient and his/her matched healthy control (10 pairs in total). This minor change was necessary in order to accommodate dependence induced by matching. As in the case of patients only, the fixed effects consisted of electrode positions and electrical current states, in addition to the group (patient versus control).
Model parameters were estimated via the restricted maximum likelihood method (REML), and parameters were considered statistically significant if the \(P\) value of their corresponding likelihood ratio (LR) tests was smaller than 0.05. All statistical analyses were performed using SPSS version 16.0 software (SPSS Inc., Chicago, IL, USA).

### Results

#### Demographics

Ten mentally competent dysphagic patients (3 women, 7 men) with a diagnosis of idiopathic Parkinson’s disease and ten healthy control subjects matched for age and gender were included. The mean age of the patients and the healthy subjects was 66–65 years, respectively, with a maximum age difference of 4 years between patient and matched control. The H & Y scale ranged from mild to moderate (median = II). The demographics of the patients and the healthy control subjects are presented in Table 1. The patients had their Parkinson’s disease from 5 to 13 years.

#### Reliable Variables

In Table 2, all variables with good intrarater and interrater reliabilities are presented [Cronbach’s \(\alpha > 0.65\), Cohen’s \(\kappa\) index of agreement >0.60, ICC >0.60] [15]. ICCs and Cronbach’s \(\alpha\) were computed for all continuous variables. For all ordinal variables, Cohen’s \(\kappa\) index of agreement was used. Ratings on visuoperceptual ordinal variables like preswallow anterior and preswallow posterior spill, swallow hesitancy, and postswallow oral residue showed no abnormalities. It was decided to exclude these variables because of insufficient relevance to the present Parkinson patient group. The intrarater reliability was not sufficient for the variables delayed initiation pharyngeal reflex, postswallow pyriform sinus pooling, the penetration-aspiration scale, GPJo, GPCj, and UESo. When the intrarater reliability proved to be rather

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**Table 2** Variables with good intrarater and interrater reliability [15]

| Reliable\(^a\) parameters in videofluoroscopy | Name | Definition |
|---------------------------------------------|---------------------------------|-------------|
| **Temporal parameters** | VPJc (velopharyngeal junction closure) | Moment of first contact of the soft palate against the posterior pharyngeal wall (in seconds) |
| | VPJo (velopharyngeal junction opening) | Moment of separation of the soft palate and the posterior pharyngeal wall with re-entry of air in the retrolingual space from the nasopharynx (in seconds) |
| | VPJd (velopharyngeal junction duration) | \(\Delta T\) between VPJc and VPJo (in seconds) |
| | LVc (laryngeal vestibule closure) | Moment when laryngeal elevation results in making contact between the arytenoid cartilages and the underside of the epiglottis (in seconds) |
| | LVo (laryngeal vestibule opening) | Moment of separation of the arytenoid cartilages and the underside of the epiglottis with re-entry of air in the laryngeal vestibule (in seconds) |
| | LVd (laryngeal vestibule duration) | \(\Delta T\) between LVc and LVo (in seconds) |
| | UESc (upper esophageal sphincter closure) | Moment of closure of the esophagus after bolus transport (in seconds) |
| | GPJo (glossopalatal junction opening) \(\Delta T\) between GPJo and LVc (in seconds) | 
| **Spatial and temporal parameters of hyoid motion** | Vertical hyoid motion | Maximum vertical motion during swallowing act (in mm) |
| | Duration horizontal hyoid motion | Duration between initiation of swallow and moment of maximum horizontal (anterior) motion (in seconds) |
| | Duration vertical hyoid motion | Duration between initiation of swallow and moment of maximum vertical motion (in seconds) |
| **Visuoperceptual parameters\(^b\)** | Lingual pumping | Preswallow involuntary repetitive tongue movements (5-point scale, 0–4) |
| | Piecemeal deglutition | Sequential swallowing of the same bolus (5-point scale, 0–4) |
| | Postswallow vallecular pooling | Postswallow pooling in the valleculae (3-point scale, 0–2) |

\(^a\) Cronbach’s \(\alpha >0.65\) or Cohen’s kappa index of agreement >0.60, ICC >0.60

\(^b\) Lower scores refer to normal functioning and higher scores refer to more severe disability
low (Cohen’s κ index of agreement <0.60, ICC <0.60), the interrater reliability was not computed.

Effect of Electrical Stimulation

Statistical tests for electrical stimulation and/or electrode position did not reveal statistical significance for the vast majority of the VFS parameters in the patient stratum, except for the temporal variable laryngeal vestibule duration (LVd) (Fig. 3) and the spatiotemporal variable duration horizontal hyoid motion (Fig. 4). In LVd, time on average was significantly reduced in position II (electrodes are placed horizontally below the hyoid bone) compared to position III (combination of position I and II), whereas in duration horizontal hyoid motion, time was significantly increased in position II compared to position I (electrodes are placed horizontally above the hyoid bone) (Table 3). This same effect was observed for the control group (Fig. 4). The general lack of significance for electrode positions and electrical current status was strongly confirmed by the random intercept model using all data (patients and healthy control subjects), which showed that these factors did not rise above individual differences. By contrast, once adjusted for electrode position and electrical current status in the statistical model, significant group differences emerged (Table 4). In Fig. 5, for instance, box plots of the temporal variable UESc of the individual matched pairs are displayed. The objective of this illustration is twofold. First, it allows for visualization of all data (patients and healthy control subjects), highlighting the nesting of the subjects within pairs. Second, it shows that for six of the ten patient–control pairs, the patients had values that are larger than or comparable to those for the controls, resulting in the statistically significant difference observed between the two groups. The significant results of the random intercept models using patient data and all data (patients and healthy control subjects) are summarized in Tables 3 and 4, where the marginal estimated mean values for the significant fixed effects are given (the current on/off effect is omitted due to its nonsignificance).

Discussion

Studying therapy effects for dysphagia in Parkinson’s disease using surface electrical stimulation is a challenge. In previous studies, several authors have investigated the effects of surface electrical stimulation in other populations such as chronically dysphagic patients, stroke patients, or healthy subjects [3, 4, 16]. However, the pathological mechanisms of oropharyngeal dysphagia in Parkinson patients are quite different from the mechanisms of chronic dysphagia in many other diseases, e.g., dysphagia following treatment for head and neck cancer or stroke. The pathophysiology of dysphagia in Parkinson’s disease is complex and dependent on the coordination among both peripheral and central nervous system factors; uncoordinated or disrupted signals along these pathways...
and delayed initiation of the swallowing reflex [17–19]. Therapies aimed at reduction of the aspiration risk in Parkinson’s disease can include voluntary airway protection techniques and bolus modification [20–22].

In the present study, differences in swallowing physiology during a single-session protocol of surface electrical stimulation were investigated in Parkinson patients and age- and gender-matched healthy control subjects using qualitative and quantitative variables in videofluoroscopy that have proved to be sufficiently reliable (Table 2).

Poor reliability was observed for the penetration-aspiration scale, among others variables. Diverse situations may have contributed to this finding. First, despite their high level of expertise, the strict methodological protocol for repeated measurements, and the consensus training, the raters may have lacked consensus on a definition of the levels of the scale. Second, patients were found to be rather homogeneous with respect to several of the variables being measured, i.e., some variables such as preswallow anterior spill, preswallow posterior spill, and the penetration-aspiration scale almost always scored consistently the same level of the ordinal scale.

For most temporal, spatial, and visuoperceptual variables, no statistically significant changes were found during surface electrical stimulation. For the temporal variable laryngeal vestibule duration (LVD), a significant effect was found for position II (in which the electrodes are placed horizontally below the hyoid bone) compared to position III (combination of positions I and II) regardless of the status of the electrical current in the Parkinson and healthy control groups, possibly indicating a placebo effect. The value of this temporal measurement is significantly reduced in position II compared to position III, resulting in a decreased period of laryngeal closure. Although the risk of

### Table 3

| VFS parameters | Electrode position | Comparison between electrode positions |
|----------------|--------------------|---------------------------------------|
| Laryngeal vestibule duration (seconds) | Position I: | Position I versus II: NS |
| | 0.72 (0.03) | 0.03 (0.013, 0.07) |
| | Position II: | Position II versus III: Sign. |
| | 0.69 (0.03) | -0.05 (-0.097, -0.003) |
| | Position III: | Position III versus I: NS |
| | 0.74 (0.03) | 0.022 (-0.025, 0.069) |
| Duration horizontal hyoid motion (seconds) | Position I: | Position I versus II: Sign. |
| | 1.54 (0.27) | -0.737 (-1.288, -0.186) |
| | Position II: | Position II versus III: NS |
| | 2.27 (0.28) | 0.488 (-0.139, 1.116) |
| | Position III: | Position III versus I: NS |
| | 1.78 (0.33) | 0.248 (-0.379, 0.876) |

Significant VFS parameters and the estimated means plus standard errors per electrode position and the mean differences between electrode positions in combination with the 95% confidence intervals (according to the fitted random intercept models). These VFS parameters show significant differences for electrode position regardless of the electrical current status (current on/off)

### Table 4

| VFS parameters | Group | Mean (standard error) | Mean difference between patients and controls (95% CI) |
|----------------|-------|-----------------------|-------------------------------------------------------|
| Velopharyngeal junction closure (seconds) | Patients | 0.054 (0.03) | 0.059 (0.002, 0.117) |
| | Controls | -0.005 (0.03) | |
| Laryngeal vestibule closure (seconds) | Patients | 0.16 (0.06) | 0.152 (0.024, 0.277) |
| | Controls | 0.008 (0.06) | |
| Laryngeal vestibule duration (seconds) | Patients | 0.73 (0.05) | -0.32 (-0.642, -0.003) |
| | Controls | 1.05 (0.05) | |
| Upper esophageal sphincter closure (seconds) | Patients | 0.87 (0.04) | 0.07 (0.001, 0.127) |
| | Controls | 0.80 (0.04) | |
| Piecemeal deglutition (5-point scale, 0–4) | Patients | 1.248 (0.17) | 0.557 (0.235, 0.878) |
| | Controls | 0.691 (0.17) | |

Significant VFS parameters and their estimated means plus standard errors for patients and controls separately, in combination with the 95% CI of the mean difference between both groups. In the random intercept model, the data have been adjusted for electrode position and electrical current status (current on/off) which are both not significant.
pulse width of the stimulation variables may cause different effects in the stimulation variables [25]. Therefore, different values inkinson’s patients. Oropharyngeal excitability depends on session protocol of surface electrical stimulation in Par-optimal for inducing any effects during the applied single-the VitalStim electrical stimulator may not have been in measurement data.

significant differences or at least indicate possible tendencies this number of swallows and variables would reveal sig-
total), resulting in 4800 measurements. It was expected that variables were assessed per swallow (current on/off) which are both not significant

penetration or even aspiration may not be increased in the present Parkinson population, it may be increased in patients with more severe Parkinson disease due to a decreased period of laryngeal closure. For the spatially related temporal variable duration horizontal hyoid motion, a significant effect is found for electrode position II com-pared to position I (electrodes are placed horizontally above the hyoid bone), again regardless of the status of the electrical current in Parkinson patients and healthy control subjects. The value of this variable increases significantly in position II compared to position I, indicative of the hyoid motion being slowed down.

It is known that several therapies induce a placebo effect in Parkinson patients and in healthy volunteers [23, 24]. The presence of skin electrodes and the connection of the electrical stimulation device may have worked as a sham intervention. The lack of a significant effect of surface electrical stimulation in the present study may not be a simple issue of statistical power. Continuous and ordinal variables were assessed per swallow (N = 240 swallows in total), resulting in 4800 measurements. It was expected that this number of swallows and variables would reveal significant differences or at least indicate possible tendencies in measurement data.

The fixed stimulation variables (frequency = 80 Hz, pulse width = 700 μs, current intensity = 0–25 mA) of the VitalStim electrical stimulator may not have been optimal for inducing any effects during the applied single-session protocol of surface electrical stimulation in Par-kinson’s patients. Oropharyngeal excitability depends on the stimulation variables [25]. Therefore, different values of the stimulation variables may cause different effects in Parkinson’s disease. Oropharyngeal dysphagia in the presence of Parkinson’s disease can be due to dysfunction of central nervous system pathways of swallowing rather than muscle weakness or peripheral sensory dysfunction for which the applied electrical stimulation device was mainly designed for [26, 27]. The possibility that snap skin electrodes may not be a selective technique of neuromus-cular stimulation cannot be disregarded too. It is likely that muscles or other tissues not involved in swallowing physiology or antagonistic muscles (muscles that pull the hyoid bone upward or downward) have been stimulated simultaneously, thereby not resulting in a measurable effect in VFS [4]. Synchronous electromyographic (EMG) feed-back of the supra- and infrayroidal muscles was not per-formed to exclude this phenomenon. Intramuscular stimulation as described by Burnett et al. [28] provides a more precise technique of electrical stimulation, although many patients may not be willing to accept invasive elec-trodes. In addition to these explanations, the lack of sig-nificant effects may also be caused by the choice of the assessment tools as well as the outcome variables. VFS may not be the most optimal assessment tool to indicate possible effects of surface electrical stimulation in dys phagic Parkinson patients. Ertekin et al. [26] described conflicting results of radiological studies. Some of those studies did not detect any abnormalities in the swallowing of Parkinson patients, unlike other studies that found abnormalities in similar populations of Parkinson patients [26]. Furthermore, normal motility of the UES region during VFS was observed despite the presence of manometric abnormalities in the same region [26, 29]. Other assessment tools such as EMG or manometry may be more sensitive and reveal significant effects [26]. However, as the assessment protocol was already a burden on the patients, it was decided not to subject them to additional assessment tools.

Another reason for finding few significant results from the use of surface electrical stimulation can be the relatively intact swallow physiology in the early phase of Parkinson’s disease as observed in this pilot population. The population of included patients is a realistic representation of Parkinson patients who consult their speech therapists about dysphagic complaints. For several mainly logistical reasons (e.g., not being able to sit upright for VFS, condition too weak for repeated transport to the outpatient clinic for dysphagia, and suffering from Par-kinson dementia), patients with severe Parkinson’s disease, who are often admitted to nursing homes, did not find easy access to this study. On the other hand, following adjust-ment for electrode position and electrical current status in the random intercept models (Table 4), several variables show significant group differences (patients versus healthy control group) despite the early phase of Parkinson’s
dysphagic patients with Parkinson’s disease. Furthermore, potential therapeutic effect of electrical stimulation in width), or EMG feedback are necessary to evaluate the several variables.

between Parkinson patients and healthy control subjects for additional information appeared on group differences status as well as electrode positions (both not significant), adjustment in the statistical model for electrical current neural pathways involved in swallowing. Following of surface electrical stimulation and its effects on the changes measured from surface electrical stimulation can result in less efficient bolus formation, delayed oropharyngeal bolus transition, and aspiration [26, 31].

Conclusion

A single session of surface electrical stimulation using different electrode positions in dysphagic Parkinson patients during VFS resulted in only a few statistically significant effects. The present study provides preliminary data which shows that surface electrical stimulation can alter swallowing in Parkinson’s disease. However, these effects may have been caused mainly by the placebo effect. The changes measured from surface electrical stimulation were found in both healthy control subjects and Parkinson patients and the direction of change would not likely benefit swallowing. Questions arise about the mechanism of surface electrical stimulation and its effects on the neural pathways involved in swallowing. Following adjustment in the statistical model for electrical current status as well as electrode positions (both not significant), additional information appeared on group differences between Parkinson patients and healthy control subjects for several variables.

Further studies using, for example, larger patient populations, a sham intervention group, different electrical stimulation variables (frequency, amplitude, and pulse width), or EMG feedback are necessary to evaluate the potential therapeutic effect of electrical stimulation in dysphagic patients with Parkinson’s disease. Furthermore, as stated in an earlier study by Baijens et al. [15], the intrarater and interrater reliabilities in outcome studies such as this one and in future research remains a major concern. In order to determine the effects of therapy interventions on swallowing and to compare study outcomes for different subject populations, measurement protocols must be standardized and based on reproducible, reliable ratings of well-defined variables.

Disclosures The authors declare that they have no conflict of interest.

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