Advances in Retinal Imaging and Applications in Diabetic Retinopathy Screening: A Review

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ABSTRACT

Rising prevalence of diabetes worldwide has necessitated the implementation of population-based diabetic retinopathy (DR) screening programs that can perform retinal imaging and interpretation for extremely large patient cohorts in a rapid and sensitive manner while minimizing inappropriate referrals to retina specialists. While most current screening programs employ mydriatic or nonmydriatic color fundus photography and trained image graders to identify referable DR, new imaging modalities offer significant improvements in diagnostic accuracy, throughput, and affordability. Smartphone-based fundus photography, macular optical coherence tomography, ultrawide-field imaging, and artificial intelligence-based image reading address limitations of current approaches and will likely become necessary as DR becomes more prevalent. Here we review current trends in imaging for DR screening and emerging technologies that show potential for improving upon current screening approaches.

Keywords: Artificial intelligence; Deep learning; Diabetic retinopathy; Optical coherence tomography; Retina; Ultrawide field imaging

DIABETIC RETINOPATHY SCREENING PROGRAMS IN MODERN OPHTHALMIC PRACTICE

Over the past few decades, the global prevalence of diabetes in adults has nearly doubled,
increasing from 4.7% in 1980 to 8.5% in 2014, with rapid increases in middle- and low-income countries [1]. The World Health Organization projects that diabetes will be the seventh leading cause of death worldwide by 2030 [1]. Among diabetic complications, the prevalence of diabetic retinopathy (DR), diabetic macular edema (DME), and proliferative diabetic retinopathy (PDR) among individuals with diabetes is approximately 35%, 7%, and 3–7%, respectively [2–4].

Diabetic eye disease is a prime candidate for a universal screening program. It is one of the most common causes of legal blindness in developed countries, with DME and PDR being the two major vision-threatening complications of diabetes [5, 6]. Treatment before the onset of advanced DR is highly effective in preventing visual loss [7, 8]. However, patients often remain asymptomatic and do not present until advanced complications such as vitreous hemorrhage or retinal detachment develop, by which time treatment outcomes are less favorable and often incur high costs [9, 10]. A universal screening program for DR aims to identify high-risk individuals and instigate treatment before complications develop [11, 12].

The first diabetic retinopathy screening programs were implemented during the 1980s and early 1990s [13–15]. These early programs were tremendously successful in reducing the incidence of DR-related blindness. In Stockholm early DR screening efforts decreased specialist referrals for DR-related blindness by an average of 47% per year over a 5-year period following the introduction of DR screening in 1991 [14]. Implementation of DR screening in the UK had similarly impressive results, with a 49% reduction in DR-related blindness in Wales during the 2007–2015 period that was attributed to DR screening programs [16].

RETINAL PHOTOGRAPHY FOR DIABETIC RETINOPATHY SCREENING

Currently, the International Council of Ophthalmology (ICO) guidelines for DR screening include retinal examination with either (1) direct or indirect ophthalmoscopy or slit-lamp biomicroscopy or (2) mydriatic or nonmydriatic fundus imaging with ≥ 30° mono- or stereophotography, with or without OCT. Retinal imaging review should be by an examiner sufficiently well trained to assess DR severity [17]. The level of DR classification afforded by screening programs is stipulated by the American Teleophthalmology Associations (ATA; Table 1), with category 1 providing a level of detail useful for population screening.

Fundus photography for DR screening has become widely adopted worldwide as the availability of imaging platforms increases [18, 19]. Although binocular slit-lamp ophthalmoscopy has remained a standard against which other DR screening approaches are judged, fundus photography is more cost-effective and does not require ophthalmologist consultation [20–23]. With training and adequate retinal image quality, graders can differentiate eyes with different severities of DR and identify eyes with PDR that require urgent referral for treatment. Meta-analysis of 20 studies with 1,960 participants yielded a combined sensitivity for DR screening programs of 80% in detecting no DR or PDR, more than 70% for detecting mild or moderate nonproliferative diabetic retinopathy (NPDR) and clinically significant macular edema (CSME), and 53% in detecting severe NPDR [24]. The specificity of screening programs was typically > 90% in the same study.

Improvements in fundus photography, particularly since the 1970s, have resulted in increased photographic quality and throughput that has facilitated implementation of teleophthalmology programs. Digital cameras are now approaching the potential resolution of film cameras, and digital photography is considered a reliable alternative to traditional film-based seven-field photography used in the Early Treatment of Diabetic Retinopathy Study (ETDRS) [25, 26]. Current fundus cameras have resolutions in the 20 megapixel range (e.g., Canon CR-2), which exceeds the 2–3 megapixel resolution required to display a single microaneurysm at the minimum identifiable diameter of 2–3 pixels [27]. Incorporation of image sensors in the range of 64 megapixels, however, is
required to achieve sharp focus everywhere for 45° field diameter images using standard flash photography red-green-blue (RGB) image sensors [28, 29]. At present, such cameras remain prohibitively expensive for many government screening programs.

Mydriatic and Nonmydriatic Fundus Photography

In terms of pupil dilation, there is no international consensus on the optimal approach to DR screening. Comparative trials of mydriatic and nonmydriatic fundus photography have demonstrated that mydriasis significantly reduces the proportion of ungradable photographs, from 19–26% to 4–5%, and improves both the sensitivity (77–86% vs. 81–94%) and specificity (77–95% vs. 86–98%) of DR detection compared with undilated photography [24, 30–32]. Despite this, for patient convenience and logistical reasons, many programs employ nonmydriatic photography, with mydriasis being reserved for cases where ungradable images are obtained (Table 2).

Single and Multiple Field Fundus Photography

Diabetic retinopathy severity grading, as established by the ETDRS with the modified Airlie House classification, requires a laborious process of capturing stereo photos of seven standardized 30° fundus fields encompassing a horizontal fundus viewing angle of 75°. Photos are then mounted in plastic sheets and viewed against light boards using stereo viewers at 5× magnification [33]. While this approach remains the gold standard for photographic diagnosis and grading of DR, it is clearly inappropriate for large-scale population screening [34]. Dilated single-field 45° fundus photography has a sensitivity of 76–84% and specificity of 82–92% for DR [32]. In the UK, nonmydriatic fundus cameras are used for mydriatic photography with two 45° fields (one fovea centered and one disc centered) [35]. Most other programs employ single 45° field fundus photos or two- and three-field photography for screening purposes (Table 2).

| ATA clinical validation categories | Category 1 | Category 2 | Category 3 | Category 4 |
|-----------------------------------|------------|------------|------------|------------|
| Disease characterization          | No or minimal DR | DME present | Mild, moderate, or severe NPDR | Exceeds ETDRS photos to determine DR and DME level |
|                                   | Worse than minimal DR | Severe or worse NPDR, or PDR | Early or high-risk PDR DME | |
| Clinical value                    | Screening only | Screening and risk stratification | Screening, risk stratification, and treatment recommendations | Replaces ETDRS photos in clinical or research settings |
| Current programs                  | OPHDIAT (France), EyePacs (USA), Digiscope (USA) | EyeCheck (Netherlands), NHS Diabetic Eye Screening Program (UK) | Joslin Vision Network (US), SiDRP (Singapore), University of Alberta (Canada) | None |

Table 1 Validation levels of diabetic retinopathy used by the ATA. Adapted from Tozer et al. [84] and Li et al. [85]
Optical Coherence Tomography for Diabetic Macular Edema Screening

Although many current screening programs are efficient in detecting referable DR, the accurate diagnosis of DME is more challenging. An especially problematic aspect of two-dimensional fundus photography for DME detection is the inability to reliably identify retinal thickening. The English National Screening Program (ENSP) for DR employs three photographic markers, namely (1) exudates within one disc diameter of the fovea, (2) circinates within the macula, and (3) microaneurysms or hemorrhages within one disc diameter of the fovea associated with best corrected visual acuity of worse than 6/12, as surrogates for DME [35]. This approach, while reasonable within the limits of currently used imaging platforms, has limited diagnostic accuracy. Only 17% of patients with hemorrhages or microaneurysms within one disc diameter of the fovea and reduced visual acuity had thickening on macular OCT, while only 6% had macular edema. Similarly, only 27% of those with macular exudates within one disc diameter of the fovea or circinates within two disc diameters of the fovea had thickening on...
macular OCT [36]. A cross-sectional observational study from Hong Kong recorded a false-positive rate of 86.6% for macular edema using conventional fundus photography screening methods [37]. Among eyes proven to have macular edema on OCT, approximately one quarter to one-third are missed by fundus photography screening [38].

Several studies have investigated the incorporation of macular OCT as part of a DR screening program to determine if this approach is beneficial from a medical and cost-effectiveness perspective. Prescott et al. found that use of OCT in cases where color fundus photos suggested the presence of macular edema resulted in direct cost savings of 16–17% because of fewer unnecessary referrals without a measurable decrease in medical benefits [19]. A cost-effectiveness study of DME screening in Hong Kong found that although the screening cost per patient increased by 35% if OCT was performed on all patients undergoing color fundus photography, the cost per quality-adjusted life-year was reduced by 45% (RW, unpublished). In contrast to these promising studies, more recent work from Australia that compared DR screening using a standard color fundus photography (CentreVue DRS fundus camera, Padova) with a combined fundus camera and OCT instrument (3D OCT-1 Maestro, Topcon, Tokyo) concluded that there was no added benefit of OCT [39]. This was due to the substantial increase in ungradable fundus photos obtained with the combined fundus camera/OCT scanner that required specialist referral, negating the benefit of reduced referrals for macular edema based on OCT imaging. This negative result, however, was largely specific to the scanning instrument chosen and would likely have been overcome with the use of a dedicated fundus camera and OCT scanner setup. That said, significant challenges remain to the addition of dedicated macular OCT scans to current DR screening protocols, such as the relatively low availability of OCT machines and expertise of operators in general outpatient clinics for screening due to cost constraints.

GRADING FUNDUS PHOTOS FOR SIGNS OF DIABETIC RETINOPATHY

Telemedicine Standards for DR Screening

The degree to which DR severity and thus referral and treatment urgency is assessed varies has been categorized into four levels by the ATA. Category 1 includes programs that can distinguish no or minimal DR from more than minimal DR, while category 4 enables complete categorization of DR into mild, moderate, and severe nonproliferative disease, early and high-risk proliferative disease, and whether macular edema is present (Table 2). Current DR screening programs employ ATA categories 1–3 (Table 2); as a result, the incidence of DR and DR-related blindness have fallen dramatically [35]. In tandem, the implementation of telemedicine DR screening programs is cost-effective compared with physician-based DR screening approaches and generates similar health outcomes [40].

Automated DR Image Assessment Systems

A relative scarcity of ophthalmologists necessitates the use of specially trained non-ophthalmologist and non-physician graders for DR screening. Such graders are used in most developed countries nowadays (Table 2), and previous work has demonstrated that this approach is adequate for DR detection [41–44]. Despite this, the growing prevalence of diabetes has placed greater pressure on healthcare systems to increase screening throughput while minimizing costs. Automated grading for diabetic retinopathy was reported in the 1990s, when Gardner and colleagues described the use of an artificial neural network capable of detecting diabetic retinopathy with 88% sensitivity and 83% specificity relative to an ophthalmologist [45]. Their system and others like it employed pattern recognition algorithms trained to identify specific retinopathy features, such as microaneurysms, and as such required time-
consuming pre-processing of training images to
isolate clinically important features and develop
mathematical descriptors of different lesion
types.

Deep Learning (DL) is a new iteration of
artificial intelligence (AI) that employs con vo-
lutional neural networks (CNNs) to interpret
images by repetitive analysis and comparison
of the output with a standard (i.e., a human gra-
der) and self-correcting if an error is made. DL is
made possible by recent advances in software
programming, the availability of large data sets
used to train image recognition software, and
high-resolution digital imaging systems
[46–50]. Multiple studies have shown successful
results in developing DL algorithms that are
capable of identifying referable DR without the
prior need to teach the computer systems
specific features of DR. The sensitivities and
specificities of these approaches are in general >
90% and 95%, respectively [44, 47–49]. Import-
antly, the negative predictive value of current
DL algorithms for DR detection is now upwards
of 99%, with less than 1% probability of missing
severe NPDR, PDR, or macular edema [51].
Current generation DL algorithms that employ
standard color fundus photos have already
achieved grading performance similar to retinal
specialists [52, 53]. A large-scale trial of a DL
algorithm trained for DR screening with a
multi-ethnic data set also included additional
algorithms for detection of glaucoma and age-
related macular generation (AMD) [48]. Detec-
tion of possible glaucoma had a sensitivity of
96.4% (95% CI 81.7–99.9%) and specificity was
87.2% (95% CI 86.8–87.5%), while detection of
possible AMD achieved a sensitivity of 93.2%
(95% CI 91.1–99.8%) and specificity of 88.7%
(95% CI 88.3–89.0%). More recently, DL
approaches were even used for automated
interpretation of macular OCT scans and
demonstrated diagnostic accuracy exceeding
that of trained ophthalmologists for a variety of
macular diseases including DME [54].

Several DL algorithms for DR screening,
including the recently FDA-approved IDx-DR
algorithm [51, 55], have been reported. These
can broadly be grouped into lesion-based dis-
ease detection systems and image-based (“black
box”) detection systems. Lesion-based systems
are trained using known disease features of DR
such as microaneurysms, blot hemorrhages, and
exudates. In contrast, black box disease detec-
tion systems, such as the Google Brain system
[47], are trained using fundus photographs that
have been graded for DR, but the specific
pathologic features being detected by the algo-
algorithm remain unknown, and output is given
simply as a positive or negative response to a
disease state.

Clearly DL approaches hold great promise for
rapid, reliable, and cost-effective screening for
diabetic retinopathy. However, several impor-
tant challenges remain that complicate the
introduction of these algorithms into large-scale
screening programs. Despite the impressive
performance previously reported by the Google
Brain team using an image-based DR detection
system, recently presented work from Lynch
et al. [56] revealed that this “black box”
approach to DR screening is highly vulnerable
to seemingly innocuous alterations of fundus
images. Using a series of reference DR fundus
photos containing typical features of DR, slight
pixel modifications (0.12–0.51% of total pixels)
were introduced into the images that were
essentially imperceptible to human readers and
did not obviously alter the appearance of the
DR lesions. These altered photos were then
presented to an image-based CNN previously
trained with half a million DR photos. The
modified images were classified as normal by
the image-based CNN, while the lesion-based
system still detected DR. In light of this work,
the potential value of image-based CNNs in
identifying novel fundus signs of DR needs to be
balanced against their potential failure to detect
clinically obvious disease.

Another limitation of many current DL
approaches is the binary nature of algorithm
development. Most contemporary CNNs are
trained using normal fundus images and images
with a single disease, such as DR. The variety of
retinal pathologies and differences in referral
urgency make this approach inappropriate in a
typical heterogenous population that would
attend retinal screening programs. A recent
attempt to use contemporary CNNs trained
with a variety of retinal pathologies, including
DR, AMD, vein and artery occlusions,
hypertensive retinopathy, Coats disease, and retinitis, found that diagnostic accuracy for any particular pathology dropped precipitously with each additional disease added to the diagnostic algorithm, to as low as 20–30% after the addition of ten distinct retinal pathologies [57]. It remains to be seen whether these limitations will be overcome with the development of more sophisticated DL algorithms and more powerful computer hardware. Additionally, the usefulness of algorithms trained using retinal images from a particular population may not extend to other populations [48]. While the clinical findings of DR are largely similar between races, it is possible that DL algorithms are also recognizing new DR markers that are not shared among different populations.

EMERGING IMAGE MODALITIES FOR DR SCREENING

Ultrawide-Field Imaging for Diabetic Retinopathy Screening

The narrow field of view in ordinary fundus photographs (e.g., single-field 45° or even a 7-field standard ETDRS) may exclude peripheral DR lesions. This is significant when predominantly peripheral lesions (PPLs) are associated with retinal ischemia, DR progression, and development of proliferative retinopathy [58, 59]. Eyes with PPLs were shown to have a 3.2-fold increased risk of two-step or more DR progression and a 4.7-fold increased risk for progression to proliferative disease [58]. Ultrawide-field (UWF) imaging, which can image 80% of the retinal surface, is therefore an important imaging modality for DR screening. Use of UWF imaging for DR screening can achieve a sensitivity up to 99% and specificity up to 97% for DR [34]. The Optos (Daytona, Optos) and Clarus 500 (Carl Zeiss, Oberkochen) are currently available UWF imaging platforms that both enable 200° field retinal imaging in only one or two images.

Optos is a scanning laser ophthalmoscope that produces retinal images of up to 200° in non-mydriatic eyes [60, 61], representing more than three times the retinal surface of traditional ETDRS seven-field photos [62]. Such images enable identification of peripheral retinal lesions of diabetic retinopathy that cannot be seen on conventional fundus photos [60] (Fig. 1). The recently released Clarus 500 captures 133° fundus photos or 200° composited photos but, unlike Optos, is able to produce true-color images that may potentially enable more accurate identification of DR lesions, although this has yet to be demonstrated in clinical trials.

The rate of ungradable fundus photos, a common cause of specialist referral in DR screening programs, was dramatically reduced when non-mydriatic UWF was employed compared with conventional non-mydriatic multifield color fundus photography in a US-based DR teleophthalmology program involving over 25,000 patients [63]. An ungradable rate per patient for DR was 2.8% with Optos UWF compared with 26.9% with multifield photography, while the ungradable rate for DME was 3.8% with Optos UWF compared with 26.2% with multifield photography. Overall, the study demonstrated an 81% reduction in ungradable fundus photos and almost twofold increased DR detection.

At present, the major constraint to widespread adoption of UWF systems such as the Optos and Clarus for DR screening programs is largely financial—such instruments cost an order of magnitude more than conventional fundus camera setups. Despite the impressive

![Fig. 1](https://example.com/fig1.png)

**Fig. 1** Comparison of standard 45° fundus photography and ultrawide-field imaging of diabetic retinopathy using the Optos imaging platform (Optos, Daytona, IL). a Diabetic retinopathy with macular edema, imaged using a 45° field fundus camera; b the same eye following panretinal photocoagulation, imaged with the Optos ultrawidefield imaging platform
outcomes of clinical trials, it remains unclear whether the cost savings of reduced inappropriate referrals are sufficient to justify the financial outlay [64].

OCT Angiography as a Screening Tool

OCT angiography (OCT-A) is a novel noninvasive imaging modality that can detect blood flow within the retina (Fig. 2). In diabetic retinopathy, microaneurysms and retinal neovascularization can be detected using OCT-A noninvasively [65]. Although the clinical utility of OCT-A remains to be established [66], several recent works have highlighted its potential for incorporation into DR screening approaches. Accurate noninvasive grading of DR severity by OCT-A analysis has been demonstrated via analyses of foveal avascular zone acircularity [67] and retinal plexus densitometry [68–70]. Automation of OCT-A image analysis has also been used for quantitative assessment of DR vascular changes that correlate with visual acuity and may be useful for monitoring DR progression [71].

Portable Fundus Photography for Detection of Diabetic Retinopathy

Modern digital color fundus cameras, although widely available in developed regions, still typically cost many thousands of dollars, are large and cumbersome, and require specially trained ophthalmic photographers. This often limits their deployment in developing regions and in areas with underserved patient populations who are less likely to attend regular ophthalmic screening. In recent years, several manufacturers have attempted to address this problem by developing fundus photography attachments for smartphones with digital cameras. Modern smartphone cameras are capable of producing very high-quality digital images the match or exceed the resolution of dedicated clinical-grade retinal cameras, albeit with smaller image sensors. Contemporary smart phones feature ≥10 megapixel wide-angle and telephoto cameras with optical image stabilization and are a potentially useful alternative to conventional fundus cameras.

Fundus photography using a smartphone and handheld 20-diopter condensing lens has been successfully used to capture fundus photos

Fig. 2 Wide-field OCT angiograms of diabetic retinopathy using image montaging captured using the Plex Elite 9000 swept-source OCT angiography platform (Carl Zeiss AG, Oberkochen, Germany). Retinal swept-source OCT-A slabs demonstrate mild non-proliferative diabetic retinopathy with intact retinal vasculature (a) and moderate non-proliferative diabetic retinopathy and multiple foci of capillary fallout seen in the temporal macula and beyond the vascular arcades (b)
and since then several commercial developers have released hardware attachments and software to enable convenient fundus photography. Current smartphone-based imaging solutions are based on the incorporation of additional lens elements in line with the smartphone camera and typically come with custom software that enables capture, labeling, and secure transmission of fundus photos. Outcomes of recent prospective clinical trials with smartphone-based fundus photography systems used for DR screening are summarized in Table 3. In most reports the sensitivity for DR using images captured from smartphones is comparable to slit-lamp biomicroscopy or dedicated fundus camera imaging with the benefit of far greater affordability.

Given the obvious benefits of low cost and portability, there is clearly excellent potential in smartphone-based DR screening, though the questionable ability of these imaging systems to provide fundus images through undilated pupils poses a problem for screening programs that do not employ routine dilation. Concerns about acute angle closure precipitated by dilation, particularly in East Asian populations, may render this approach undesirable in certain regions. Portable nonmydriatic fundus cameras are widely available and have been successfully tested for DR screening (Table 3), with diagnostic performance comparable to smartphone-based systems. These devices offer somewhat better diagnostic performance than fixed fundus cameras in terms of image gradeability and diagnostic accuracy, but the benefit of portability cannot be overstated. Several large trials have demonstrated the potential of these devices for detecting referable DR in developing regions. It is likely that the incorporation of both smartphone-based and dedicated

| Study                | Camera                                      | Ungradeable images | Mydriasis | Detection of DR | Standard for comparison |
|----------------------|---------------------------------------------|--------------------|-----------|----------------|------------------------|
|                       |                                             |                    |           | Sensitivity (%) | Specificity (%)        |
| Smartphone-based fundus cameras |                                             |                    |           |                |                        |
| Russo et al. [76]    | D-Eye (D-Eyecare)                           | 3.75%              | Yes       | 75–89          | 93–100                |
| Toy et al. [74]      | Paxos Scope (Verana Health)                 | 2%                 | Yes       | 91             | 99                     |
| Ryan et al. [75]     | Unmodified smartphone with hand-held 20D lens | 1.8%               | Yes       | 50             | 94                     |
| Rajalakshmi et al. [77] | Fundus-on-phone (FOP, Remidio Innovative Solutions) | None               | Yes       | 92.7           | 98.4                   |
| Dedicated portable nonmydriatic fundus cameras |                                             |                    |           |                |                        |
| Ting et al. [97]     | Eyescan (OIS)                               | 8.5%               | Yes       | 93             | 98.2                   |
| Zhang et al. [98]    | Pictor Smartscope (Volk Optical)            | 6–14%              | No        | 64–88          | 72–84                  |
| Sengupta et al. [79] | Pictor Smartscope (Volk Optical)            | –                  | No        | 88–93          | 84–90                  |
portable fundus cameras into DR screening programs will increase dramatically in the coming years, particularly in developing countries with large rural areas where clinic review is often not feasible. Recent incorporation of AI-based automatic image grading to smartphone fundus images [82] offers potential for even further improvements to the cost-effectiveness and convenience of screening programs.

CONCLUSION

Over the past few decades, diabetic retinopathy screening programs have been implemented in essentially all developed nations and many developing nations [10, 83]. While most current screening programs employ conventional fundus photography with trained grading staff, research over the past few years has demonstrated a role for newer imaging modalities and image analysis software that has the potential to improve screening accuracy and reduce the financial burden of these increasingly expensive programs. With the dramatic increase in diabetes prevalence currently occurring worldwide, it is clear that more efficient screening programs will be required not only to ensure early detection of disease, but also to reduce inappropriate referrals to ophthalmologists for non-sight-threatening disease that is more appropriately managed with continued observation in a primary healthcare setting.

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