Comparison of Depth of Cure, Hardness and Heat Generation of LED and High Intensity QTH Light Sources

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\textbf{ABSTRACT}

Objectives: To compare curing performance of a second generation LED curing light with a high power tungsten quartz halogen (QTH).

Methods: A hybrid composite resin (Filtek Z 250, 3M, USA) was used as test material and cured using a second generation LED light (Translux Power Blue\textsuperscript{TM}, Heraus Kulzer, Germany) or a very high power QTH light unit (EMS, Switzerland). A two split aluminum mold was used to prepare ten samples with LED light source cured for forty seconds and ten samples prepared using high power QTH light unit, cured for four or six seconds recommended exposure time. Hardness, depth of cure (DOC) and thermal rise during exposure time by these light sources were measured. The data submitted to analysis of variance (ANOVA), Tukey’s and student’s t tests at 5% significance level.

Results: Significant differences were found in hardness, DOC of samples cured by above mentioned light sources and also in thermal rises during exposure time. The curing performance of the tested QTH was not as well as the LED light. TPB light source produced the maximum hardness (81.25, 73.29, 65.49,55.83 and 24.53 for 0 mm, 1 mm, 2 mm, 3 mm and 4 mm intervals) and DOC (2.64 mm) values with forty seconds irradiation time and the high power (QTH) the least hardness (73.27, 61.51 and 31.59 for 0 mm, 1 mm and 2 mm, respectively) and DOC (2 mm) values with four seconds irradiation time. Thermal rises during 4 s and 6 s curing time using high power QTH and tested LED were 1.88\degree C, 3\degree C and 1.87\degree C, respectively.

Conclusions: The used high power LED light produced greater hardness and depth of cure during forty seconds exposure time compared to high power QTH light with four or six seconds curing time. Thermal rise during 6 s curing time with QTH was greater compared to thermal changes occurred during 40 s curing time with tested LED light source. There was no difference seen in thermal changes caused by LED light with 40 s and QTH light with 4 s exposure time. (Eur J Dent 2011;5:299-304)

Key words: Hardness; Depth of cure; Resin composite; Heat generation.

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Light emitting diode (LED) light curing units are becoming increasingly popular in dental practice. Most of the first-generation LED light units were unable to cure composite resin in the manner of quartz-tungsten-halogen (QTH) light sources. Since the spectral output of the LEDs is concentrated in the blue wavelength range, high power LED curing lights are capable of polymerizing some resins as well as, or better than, some QTH lights. LED curing units are characterized by a relatively narrow emission spectrum and lower heat generation than QTH curing units.

There have been reports that exposure causes less temperature rise with a conventional curing light than with an LED curing light and that higher pulp chamber temperature changes are induced by high output curing units than by conventional curing units. Likewise, previous findings that had indicated less temperature rise with LED units than with QTH units have been debated in another study.

The degree of conversion of composite resins is influenced by the spectral distribution and intensity of the curing light as well as the shade, opacity, and chemical composition of the resin-based composite. While both LED lights and quartz-tungsten-halogen lights are believed capable of curing resin-based composites, some differences are observed in the performance of the cured resin. Moreover, both the composite material and its curing time have a significant association with the resulting degree of polymerization.

It has been shown that LED light units, like conventional halogen light sources, are capable of curing the camphorquinone-based composites to an acceptable degree of polymerization and such resin composites show similar strain behavior whether an LED or halogen light curing unit is used to polymerize the resin composite. The ability to reduce exposure time by using high power LED or QTH lights may improve clinical time management.

A hybrid composite resin with A3 shade (Filtek Z250, 3M ESPE, St Paul, MN, USA) was used in this study as the test material. The curing light sources used in this study were a second-generation LED light unit with 860 mW/cm² intensity (Translux Power Blue, Heraeus Kulzer, Germany) and a very high power QTH light unit with 2890 mW/cm² (Swiss Master Light, EMS, Switzerland). The light intensity of the units was checked using the built-in digital radiometer of an Optilux 501 light curing unit.

A two-split aluminum mold with a semicircular column-shaped hole (4 mm in diameter and 8 mm deep) was used to prepare samples for measuring the depth of cure and the hardness. The mold was placed on a sheet of Mylar strip and then the resin was compressed to produce a flat surface before it was covered by a clear polyester strip (Matrix Tape Refill, 3M) and finally was photopolymerized. For the control group, a Translux Power Blue (TPB) was used in continuous light photoactivation mode for 40 s. Ten samples were prepared with the TPB light source. For the test group, a QTH light unit (EMS) was used in fast cure mode for either 4 s or 6 s. Ten samples were prepared with the EMS light source for each exposure time (4 s or 6 s). The cure depth of the resin was determined using a standard technique (ISO 4049:2000). Immediately after irradiation, the uncured material was scraped away with a spatula. The height of the cylinder of set resin was measured with a digital micrometer (Digital Cal, Switzerland) to a precision of ±0.01 mm, and the result was divided by two. Vickers hardness values were determined at 1.0 mm intervals along the depth of the cured samples, on a flat surface that was parallel to the direction of the light source, using a universal indenter (Leitz Wetzlar, Germany).

The data were submitted to analysis of variance (ANOVA) as well as Tukey’s and Student’s t tests at the 5% significance level.
RESULTS
Analysis of the data revealed significant (P<.05) differences among the samples cured by the light sources in terms of Vickers hardness, depth of cure, and thermal changes during irradiation.

Hardness
The hardness values of the 0 mm, 1 mm, and 2 mm levels all indicated significant differences between the samples cured by the TPB light unit and those cured by the EMS light unit (regardless of the 4 s or 6 s exposure time). Note that hardness values of the 3 mm and 4 mm levels were measurable only in those samples cured by the TPB light unit. Indeed, the maximum Vickers hardness values were produced by the TPB light unit, which gave 81.25, 73.29, 65.94, 55.83, and 24.53 for the 0 mm to 4 mm levels, respectively. The minimum hardness values were produced by the EMS light unit with a 4 s exposure time, which gave 73.27, 61.51, and 31.59 for the 0 mm to 2 mm levels, respectively. Between the samples irradiated by the EMS light unit for 4 s and 6 s, there was no significant difference in the hardness value at the 0 mm or 1 mm level, but there was at the 2 mm level. In samples cured with the TPB light unit, the 1 mm and 2 mm levels attained hardness values greater than or equal to 80% of the corresponding surface hardness values. In samples cured with the EMS light unit for 4 s, only the 1 mm level attained 80% of the corresponding surface hardness values. In samples cured with the EMS unit for 6 s, the 2 mm level attained hardness values that were closer to 80% of the corresponding surface hardness values than in samples cured for only 4 s (Table 1, Figure 1).

Depth of cure
The depth of cure (DOC) reached its maximum of 2.64 mm in samples cured by the LED light unit and its minimum of 2.00 mm in those cured by the QTH light with a 4 s exposure time. There was thus a significant (P<.05) difference in DOC between samples cured with the LED light unit and those cured with the QTH light unit. However, this significant difference was also found between samples cured with the EMS light unit for 4 s or 6 s of exposure time, since the DOC was 2.00 mm or 2.15 mm, respectively.

Thermal changes
There was only an insignificant (P>.05) difference between the mean temperature rise generated by a 40 s irradiation with LED light (1.87 °C, SD=0.34) and that generated by a 4 s irradiation with QTH light (1.88°C, SD=0.19). However, for a 6 s irradiation with QTH light the analogous difference (3°C, SD=0.27) was considerable. Note that the difference in temperature rise between 4 s and 6 s of irradiation with the QTH light unit was also significant.

DISCUSSION
In this study, the curing performance of a high power halogen light unit (EMS) was matched against that of a second-generation LED light unit (TPB) with the aim of determining whether the halogen light unit with its short recommended exposure time is capable of curing composites as completely as the LED light unit with its 40 s irradiation time.

In general, larger hardness values are indicators of more extensive polymerization.22 The depth of cure for light activated dental resin composites has thus often been evaluated indirectly by measuring the hardness of the material at specific depths.23,24 It has been suggested that the depth of cure be defined as the level above which the hardness value of the cured resin composite is greater than or equal to 90% (or recently 80%) of the surface hardness value.25,26

The resin composite used in this study contains camphorquinone as the photoinitiator, and generally such resin composites can be more efficiently

| Intervals | 0 mm       | 1 mm       | 2 mm       | 3 mm       | 4 mm       | DOC (mm) |
|-----------|------------|------------|------------|------------|------------|----------|
| TPB       | 81.25 (1.61)| 73.29 (0.88)| 65.49 (1.00)| 55.83 (1.40)| 24.53 (6.05)| 2.44     |
| EMS (4s)  | 73.27 (1.17)| 61.51 (0.86)| 31.59 (0.39)| -          | -          | 2        |
| EMS (6s)  | 73.74 (0.78)| 62.16 (1.02)| 53.52 (1.01)| -          | -          | 2.15     |

Figure 1. Vickers hardness values of resin composite at different intervals cured by different light sources and exposure time.

Table 1. Vickers hardness values in different intervals and DOC of resin composite cured by light sources. SD is given in parenthesis.
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cured using LED light units. From 78% to 95% of the light emitted by a blue LED unit is within the wavelength range 450–500 nm, as opposed to 56% for a conventional halogen unit. Therefore, only light within this range can best activate camphorquinone. However, some studies have indicated that a longer curing time is needed to reach a similar depth of cure and to create optimal performance for resin composite materials when using an LED light unit rather than a conventional tungsten halogen light unit.

For a given irradiation time, it can be anticipated that the microhardness of the composite decreases as the thickness of resin cured increases. In this study the LED light gave better performance than the high power halogen light with respect to hardness and depth of cure. In samples cured with the LED (TPB) light unit, the 1 mm and 2 mm levels attained hardness values greater than or equal to 80% of the corresponding surface hardness values. However, in the samples fast cured with the QTH (EMS) light unit, only the 1 mm levels attained 80% of the surface hardness values. The wavelength range of the LED light used in this study was 440–480 nm, which explains why greater degrees of hardness and conversion were achieved by this LED light with a 40 s irradiation than by the QTH light with either a 4 s or 6 s irradiation.

The halogen curing light produced significantly lower depth of cure (DOC) and hardness values than the LED curing light. Although the QTH light unit delivered a much greater power density, suggesting a higher degree of polymerization, the LED light benefited from a much longer exposure time. The QTH light unit was only partly able to compensate for this difference, increasing the DOC but not the hardness of the resin composite. This result may be due to the reduced photoactivation time used by the EMS unit, representing a lower amount of energy and a shorter period of exposure time, such as when using the EMS unit, shortens the pregelation phase and prevents a slow and ordered chain growth.

According to manufacturer information, Filtek Z250 contains filler particles that range in size from 0.01 to 3.5 μm. Most activation light sources that are commercially available have a peak in the range 450–500 nm. Research has shown that light scattering in the resin composite is maximal when the filler particle size is half the wavelength of the activating light, resulting in a lower transmission coefficient and smaller depth of cure. The transmission coefficient is influenced by the wavelength of the light, the refractive indices of the resin and fillers, and the nature and amount of the filler particles. In comparison with the LED light, the EMS light has a much greater light intensity, which actually increases light scattering and light attenuation, resulting in less camphorquinone activation and resin conversion. This may also partly explain the decreased DOC in the samples cured with the EMS light in this study.

The light intensity and exposure time are known to be the most important factors in temperature change. Moreover, the temperature rise is known to increases with the power density of the LED or QTH unit, but yielding a greater rise for a given power density when using a QTH unit, as corroborated by the findings of this study.

Another study indicated that photocuring blue light sources increase the temperature in tooth tissue during in situ polymerization of resin composite and that a higher power density QTH light source (Swiss Master Light) caused a greater increase in tooth temperature than a high power LED light. The temperature rise was greater with increased exposure time, as found in this study as well.

In this study, increasing the period of irradiation with the QTH light from 4 s to 6 s only affected the DOC of the resin composite and the hardness of its 2 mm level. This can be partly attributed to a temperature rise by from 1.88°C to 3°C while curing the resin composite.

The thermal variations that occur during the photoactivation of composite resins are related both to the exothermic polymerization of the materials and to the heat output from the dental curing light units. A cured composite, such as the cured composite disc in this study, is capable of
reducing the ability of irradiated light to increase temperature. This has been shown by a study in which the temperature rise caused by irradiation was less via a previously cured composite than via an initially unpolymerized composite.\(^\text{39}\)

According to the results of this study, composite increments less than 2 mm in thickness should be cured using a high power QTH light source for a short period of time, especially in deep cavities to ensure proper curing of the composite. Applying thicker increments and increasing the exposure time to compensate will increase temperature rise and endanger pulp chamber vitality.

**CONCLUSIONS**

- Hardness values produced were greater with the LED light than with the QTH light.
- Depth of cure obtained was higher with the LED light.
- Depth of cure produced by the QTH light was higher for a recommended 6 s irradiation than for a shorter 4 s exposure.
- Thermal changes were greater using the QTH light for 6 s than using it for 4 s or the LED light for 40 s.
- Thermal changes were the same whether using the LED light for 40 s or the QTH light for 4 s.

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