Vitamin E as a Functional and Biocompatibility Modifier of Synthetic Hemodialyzer Membranes: An Overview of the Literature on Vitamin E-Modified Hemodialyzer Membranes

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Abstract
Along with one century of history, research has provided many solutions for hemodialysis (HD) biomaterials, encompassing several generations of copolymers that have found wide application in the development of hollow-fiber dialyzer membranes. Polysulfone-based biomaterials have gained increasing consideration and are now the gold standard in the production of biocompatible hemodialyzers. However, even the highest biocompatibility now available cannot exclude that dialyzer membranes and the overall extracorporeal circulation may produce at the subclinical level immunoinflammatory reactions and thus an increased cardiovascular risk of patients on regular HD therapy. The lipophilic antioxidant and radical scavenger vitamin E has been used (as α-tocopherol) to modify cellulosic and synthetic hollow-fiber membranes with the ultimate goal to neutralize harmful reactive species and to mimic lipid structures of blood cell plasmalemma and lipoprotein particles. Besides filtration and biocompatibility, this modifier has introduced a third function of dialyzer membranes, namely ‘antioxidant bioactivity’. Vitamin E can also serve as a template molecule to produce synthetic redox-active and -silent (non-antioxidant) modifiers for future generations of dialyzer membranes. This mini-review article describes the evolution of vitamin E-derived copolymers as a generation of biomaterials that has offered a clinical challenge and still represents a chance to further improving the quality of HD therapy.

Introduction: The Road from Biocompatibility to Bioactivity

The concept of biocompatibility with its different definitions remains central to the effort of the biomaterial industry and clinicians to provide high-quality hemodialysis (HD) therapies. Operational aspects may lead to consider biomaterials as ‘inert surfaces’ that implies ‘the lack of any perturbation’ [1] during the contact between blood and the dialysis membranes or alternatively as an interacting body in which the definition of ‘sum of specific interactions’ [2] describes a more realistic view. This latter definition paves the way for an extension of the functional chart of hemodialyzer membranes that beside
filtration and biocompatibility may include bioactivity as a third feature (Fig. 1, left panel).

The absorption of peptides and proteins such as β2-microglobulin, cytokines and modified albumin is an example of how the interaction of HD membranes and blood constituents could be desirable rather than a problem. On the other hand, protein adsorption by the blood-membrane interaction has an impact on solute removal [3] and it cannot be ruled out that this could interfere with the structure/activity of normal or uremic solutes that include abnormal plasma proteins and small molecules such as the broad family of reactive carbonyls described below in this review paper. In that way, the dialyzer membrane may entrap on the blood surface solutes that reach high relative concentrations to become more available for the interaction with blood cell receptors and plasma proteins. These may result in untoward reactions and activation processes such as those described for components of the complement and coagulation pathways [4].

Further criteria to define the concept of biocompatibility ground on clinical classifications. Acute and chronic symptoms on the dialysis patient are the ‘signature’ of a bioincompatible material and the extent of these can predict the clinical outcome of a treatment. Biological and clinical signs of poor biocompatibility are consequent to immunoinflammatory and vascular reactions (see following section). Synthetic biomaterials with higher biocompatibility have constrained these effects to subclinical symptoms (essentially revealed by biochemical tests such as cytokines and acute-phase markers) thus contributing to alleviate long-term clinical consequences of HD therapy and uremia, such as protein catabolism and malnutrition [5] and a number of other chronic effects recently reviewed in [2]. Given the role that chronic inflammation and malnutrition play as risk factors for cardiovascular disease of chronic kidney disease (CKD), the use of biocompatible dialyzer membranes is expected to influence the cardiovascular outcome of patients on regular HD therapy, which is an assumption needing further support by randomized clinical trials [6].

However, even the highest standard in biocompatibility now available cannot avoid that dialyzer membranes and the entire extracorporeal circulation would provide immunoinflammatory reactions and chronic challenges to blood vessels.

Fig. 1. 3D functional projection (right) and schematic structure (left) of the composite PS-polyvinylpyrrolidone copolymer of vitamin E-modified hemodialyzer membranes (VitabranE®).
Poor biocompatibility of dialysis therapies results in proinflammatory, prooxidant stress and prothrombotic events. Accordingly, the repeated contact of patient’s blood with the materials of the extracorporeal circulation causes oxidative stress biomarker formation, changes in the levels of inflammatory and anti-inflammatory cytokines (such as IFN-γ, TNF-α, interleukin (IL)-1β, IL-4, IL-6, IL-10, IL-12 and IL-18), acute-phase (C-reactive protein (CRP), SSA and fibrinogen) and negative-phase (serum albumin, prealbumin and transferrin) proteins, and leukocyte subsets, which reset to a dysfunctional immuno-inflammatory phenotype [recently reviewed in 7]. Other consequences of bioincompatibility are the activation of complement and contact pathways [4, 8], and platelets [9]. Indices of red blood cell damage can represent other useful markers of biocompatibility [7, 10, 11].

The material of the hollow-fiber dialyzer membrane is the key player of blood cell activation together with bacterial contaminants in the dialysis fluids, which eventually come into contact with the patient’s blood throughout the same dialyzer membrane. Vitamin E, as α-tocopherol (α-TOC) (fig. 2), has been used to modify both cellulosic and polysulfone (PS) copolymers that are now available to produce hollow-fiber hemodialyzer membranes [recently reviewed in 12, 13] (fig. 1, right panel). This vitamin is used as a coating agent for HD biomaterials with the ultimate goal to mimic lipid structures of blood cell plasmalemma and lipoprotein particles, and to neutralize harmful reactive oxygen species (ROS). In fact, vitamin E is a well-known lipophilic antioxidant and a scavenger of hydroperoxyl radicals. Besides filtration and biocompatibility, this latter effect expands the functional definition of dialyzer membranes to a new dimension, i.e. that of ‘antioxidant bioreactivity’ described above and in the left panel of figure 1. Another example of this concept in HD biomaterials was that of heparin-grafted HD membranes [14]. Vitamin E can also be used as a template molecule to produce redox-silent (non-antioxidant) modifiers. Recently, Δ-α-tocopheryl polyethylene glycol (PEG) 1000 succinate (TPGS), an esterified form of α-TOC (fig. 3), was used to synthesize a PS-based copolymer, which appears to have improved in vitro biocompatibility and filtration performance [15].

These generations of vitamin E-derived copolymers have generated a new clinical perspective in HD therapy by developing more biocompatible biomembranes and even functional (redox-active) biomaterials. Early studies have provided preliminary clinical evidence in support of a clinical superiority of vitamin E-derived copolymers with respect to other synthetic biomaterials such as PS, which represent the gold standard in the production of cost-effective hollow-fiber hemodialyzers. Further and structured trials are awaited to achieve solid evidence.
This review paper provides a critical examination of the literature so far produced on vitamin E-bonded dialyzer membranes.

**Bioincompatibility, Microinflammation and Oxidative Stress: Clinical and Biochemical Grounds**

Endothelial cells and the other cell components of arteries appear to have the greatest susceptibility to the challenging effects of chronic inflammation of CKD [reviewed in 16, 17]. This may explain the increased cardiovascular morbidity and mortality of HD patients and the possible relationship with a poor biocompatibility of dialysis therapies [reviewed in 6].

Endothelial cells are highly prone to oxidative stress that can be prevented both in vitro and in vivo by antioxidants and mitochondrial protection agents [18–20]. ROS and receptor-dependent effects of cytokines and modified low-density lipoprotein (LDLs) are associated with an impaired energy function and apoptotic signaling of mitochondria, and cause ER stress through either Ca-dependent or -independent signaling in different types of cells [21, 22]. At the same time, ROS and the binding of oxidized LDL (Ox-LDL) to scavenger receptors of endothelial cells activates the proinflammatory transcription factor as NF-κβ [23, 24], inhibits the transcriptional activity of PPAR-γ [25] and causes the accelerated senescence of endothelial progenitor cells [22]. These events altogether may sustain vascular microinflammation, arterial calcifications and atherosclerotic plaque formation by means of different underlying events such as (1) a defective capability of the arterial wall to prevent lipid deposition and foam cell formation, (2) a lowered capability to regulate the remodeling of the extracellular matrix and calcium deposition, (3) impaired mechanisms of prevention of leukocyte and platelet activation, and (4) poor repair of endothelial cell damage.

If these factors promote the formation of inflammatory lesions of the main vessels, other tissues such as the skeletal muscle and liver undergo a series of changes mediated by cytokines such as TNF-α and IL-6. These also sustain a negative protein metabolism in these tissues, which is a major causal event in CKD malnutrition [26] and may also contribute to insulin resistance [27]. Lipid peroxidation by-products such as oxysterols and 4-hydroxynonenal conspire with direct effects of oxidation to impair the endocrine and paracrine function of the adipose and skeletal muscle. These products may affect the levels and lipotoxicity of free fatty acids and adipokines and ultimately may cause insulin resistance. A defective insulin signaling impairs the endothelial metabolism of nitric oxide and the activity of plasminogen activator inhibitor-1, which together with platelet activation, increase thrombogenicity in patients treated with bioincompatible materials. RBC rheology may change upon bioincompatible treatments further increasing cardiovascular risk.

Oxidative and non-oxidative events triggered by the extracorporeal treatments are believed to influence the entire uremic comorbidity. Beside cardiovascular disease, chronic inflammation contributes to uremic anemia by lowering the responsiveness to erythropoietin-stimulating agent (ESA) and erythrocyte life span [28, 29]. Leukocyte activation and oxidative stress are also reported to cause erythrocyte damage that is sustained by shear stress and other mechanical injuries.

The repeated activation of leukocytes by the contact with bioincompatible membranes is a cause of leukopenia [30, 31] and is a leading cause of the defective cell-mediated immune response of HD patients that is associated with the conversion of lymphocytes from Th1 to Th2 phenotype and with an overproduction of inflammatory cytokines [7].

The release of pyrogens and bioactive mediators such as the vasoactive components histamine and bradykinin contribute to fever and intradialytic hypotension which are other common intradialytic events associated with the treatment with bioincompatible materials [reviewed in 32, 33].

Chronic challenges to the immune system by bioincompatible dialysis therapies can worsen the prognosis of CKD patients leading to a condition of systemic microinflammation. A self-feeding mechanism with activation loops centered on leukocytes and vascular cells has been proposed to explain the pathogenesis of CKD microinflammation [16]. These loops are fed through the same products of inflammation, i.e. cytokines and ROS [34], which per-
petuate the stimulation of inflammatory and vascular cells in combination with uremic factors and with the abnormal generation of by-products of ROS and carbonyls [35].

The burden of oxidative stress-derived by-products in CKD is higher than in other conditions of chronic inflammation, reaching the highest levels in end-stage renal failure patients. In CKD, unsaturated lipids show higher than normal oxidizability when exposed to peroxidizing agents [36–38] and plasma proteins show signs of damage by endogenous pro-oxidants, nitrative/nitrosative agents, and carbonylation by the reaction with lipid oxidation and glycation by-products [reviewed in 17, 34, 39–41]. Small solutes such as reactive carbonyls and larger solutes such as post-translational modifications of proteins, form a plethora of uremic solutes and immunoinflammatory mediators that contribute to sustain microinflammatory loops with different and only partially understood mechanisms. These solutes are the expression of a component of the uremic toxicity that is largely unaffected by the current dialysis strategies [42]. In fact, diffusive, convective or mixed techniques provide poor removal of middle to large solutes generated by the action of ROS and reactive carbonyls [reviewed in 34, 43–46].

In the end, these proinflammatory solutes sustain cell and tissue reactions through receptor-dependent and -independent mechanisms of scavenging that are responsible of the endogenous metabolism of these by-products. Modified apolipoproteins and other plasma proteins bearing post-translational modifications, such as glycated albumin [47], are scavenged by the activity of specific surface receptors, such as RAGE and the homologue CD36 that is mainly involved in Ox-LDL scavenging. These receptors are expressed in mononuclear leukocytes, neutrophils and endothelial cells, e.g. the same cells that upon stimulation produce ROS, inflammatory cytokines, chemokines, adhesion molecules and acute phase mediators, and provide the ultimate explanation to the self-feeding loop that sustains the microinflammatory syndrome of HD patients [34].

Bioincompatibility of prototypical dialyzer membranes made of regenerated cellulose has been associated with the contact of blood components with the hydroxyl groups of the β-D-glucose structure. These groups trigger intradialytic activation of the complement system and cause leukopenia [31]. Based on this burden of knowledge, two major approaches have been adopted to improve the biocompatibility of regenerated cellulose dialyzer membranes. One was chemical modification of the hydroxyl groups, e.g. modification by acetylation to obtain triacetate cellulose or with PEG chains to obtain PEG-grafted cellulose. The other, and more successful, approach was based on the development of synthetic polymer membranes such as PS or polyether sulfone membranes, which have no bioincompatible groups in their chemical structures [48, 49]. Nowadays, high-flux synthetic membranes are more frequently used and represent a cost-effective solution with proven clinical superiority over cellulosic membranes.

At the same time, symptomatic approaches have been proposed on the side of oxidative stress. Antioxidants such as vitamins C and E, and glutathione, have been used as oral supplements in an attempt to correct the progressive decrease of blood antioxidants and to alleviate the abnormal generation of ROS of HD patients [reviewed in 35] (fig. 4). In fact, CKD is a condition of antioxidant deficiency and particularly of water-soluble antioxidants (such as vitamin C) that undergo chronic leakage by the HD treatments. CKD is also a condition of higher antioxidant demand by the proinflammatory and oxidative stress environment described in the previous sections. This higher demand can be deduced by the higher susceptibility to lipid oxidation of uremic plasma and the decreased content of blood cell antioxidants [36, 50]. Few studies, however, provided solid evidence of a clinical advantage of the oral administration of antioxidants. The most convincing evidence came from the randomized clinical trial on vitamin E supplementation in HD patients known as the ‘SPACE study’ [51] that demonstrated a significant reduction (54%) of the primary endpoint (a composite variable including myocardial infarction, ischemic stroke, peripheral vascular disease, unstable angina) and 70% reduction in myocardial infarction. To confirm CKD as an elective condition for antioxidant therapy, other successful small-scale trials have been reported in CKD [reviewed in 11, 74].

One of the most original approaches of the antioxidant therapy in HD involved the use of vitamin E (fig. 2), a well-known lipophilic antioxidant, as a modifier of the surface of the dialysis membrane that is described in the
following sections. The bonded vitamin E on the surface of the dialyzer membrane is expected to reduce the production of ROS at the site where blood cells come into contact with the dialyzer membrane, thereby providing antioxidant protection in a timely and targeted manner. Because of this, two generations of vitamin E-coated dialyzers, namely cellulosic- and synthetic polymer-based membrane dialyzers, were successfully developed and launched on the market in the last two decades.

**General Concepts on Biology and Chemistry of Vitamin E**

Vitamin E was discovered in 1922 when Evans and Bishop [52] described a ‘substance X’ essential for rat fertility. A family of 8 structurally related compounds (4 tocopherols and 4 tocotrienols) is included under the name of vitamin E. Their basic structure is that of tocopheranols (fig. 2, lower structure) that in the prototypal form of \( \alpha \)-TOC brings a 6-hydroxychroman moiety and a phytol side chain attached at carbon 2 (fig. 2, upper structure). Tocopherols contain saturated side chains and three asymmetric centers (positions 2, 4’ and 8’) while tocotrienols (fig. 2, middle structure) have 3 double bonds in the positions 3’, 7’ and 11’ and one asymmetric center (position 2). The methylation pattern of the chroman ring gives origin to 4 homologues in both the tocopherol or tocotrienol families identified with the Greek letters \( \alpha \), \( \beta \), \( \gamma \), and \( \delta \). Natural tocopherols (and tocotrienols) show right-handed configuration (R) in all the asymmetric (or chiral) centers, and thus are identified as RRR optical isomers, while synthetic forms are racemic mixtures (as the all-rac-\( \alpha \)-TOC included in many vitamin E supplements) containing all the different combinations of the R and left-handed (S) optical configurations.

Humans and animals are unable to synthesize vitamin E and must obtain it from plant sources (vegetable oils, dressings, shortenings and margarines) that often contain at the same time various members of the vitamin E family [53]. Vitamin E, like cholesterol, is found in almost all organs. Approximately 3 g of vitamin E is stored in the body of a healthy adult. The main reserves are in subcutaneous fat, muscles, and the liver. The concentration of vitamin E per gram of tissue is high in adipose tissue (150 \( \mu \)g/g), in the adrenal glands (132 \( \mu \)g/g), in the pituitary or hypophysis (40 \( \mu \)g/g) and in the testes (40 \( \mu \)g/g).

Since its discovery, \( \alpha \)-TOC has been considered the most important molecule of vitamin E family [54]. It is the most abundant form of vitamin E in blood and several tissues, followed by \( \gamma \)-TOH, while the other vitamins are present only in traces. At the same time, \( \alpha \)-TOC
proves more active than any of the other ‘non-α’ homologues when assessed with several biological tests. Indeed, the biological activity calculated by the classical test of fetal reabsorption in the rat gives values ranging from 100% for α-TOC to 30% for β-TOC and 1.4% for δ-TOC \[55\]. Nowadays, vitamin E supplements almost exclusively contain α-TOH. Emerging evidence is demonstrating the different contribution of minor forms, such as γ-TOH and tocotrienols, in the biological responses elicited by the vitamin E family of compounds \[reviewed in 54, 56–58\]. These include anticancer, anti-inflammatory and immunomodulatory effects, lipid-lowering and neuro-protection functions.

One of the key biological roles of vitamin E is that of a physiological liposoluble antioxidant trapping peroxyl radicals and other reactive species generated during cell metabolism and oxidative stress \[59, 60\]. Antioxidant roles of vitamin E are influenced by the composition of the reaction medium which may provide different chemical interactions for instance with targets and particularly with co-antioxidants that include other lipophilic and hydrophilic antioxidants with biological relevance in cells and biological fluids such as ascorbic acid and glutathione \[61, 62\]. Therefore, the study of the chemistry of vitamin E oxidation is of considerable interest in connection with its mode of action and physiological relevance. The one-electron oxidation of α-TOH provides the production of a tocopheroxyl radical that can further react with lipid peroxides, leading to the formation of 8-substituted tocopherones (hydroxy- or alkyl dioxy tocopherones), tocopheryl quinone (TQ), epoxyquinones (TQE1 and TQE2) and eventually tocopherol hydroquinone \[63\].

The analysis of these compounds has been used to give a measure of the oxidation of membrane lipids and also to test antioxidant activity of vitamin E-modified hollow-fiber dialyzer \[64\].

### Vitamin E-Bonded Dialyzers

#### Development of Cellulose-Based Vitamin E-Bonded Dialyzer Membranes

In 1990, cellulose-based vitamin E-bonded dialyzer membranes were developed and introduced on the market by Terumo Corporation under the commercial name Excebrane™. The base membrane was regenerated cellulose hollow fiber, and the surface of the hollow fiber was covalently modified by hydrophilic polymers as well as oleic alcohol; then, vitamin E (α-TOC) was bonded to oleic alcohol via hydrophilic interaction. Sasaki et al. \[65\] reported the outline of the production process as well as the results of in vitro and in vivo studies on Excebrane, which showed much better biocompatibility than the original regenerated cellulose membrane.

**Clinical Outcome of Cellulose-Based Vitamin E-Bonded Membranes**

Early trials using Excebrane indicated positive clinical effects \[reviewed in 13, 32, 66\]. Reduction of oxidative stress and inflammation was described as the possible therapeutic effect. Cardiovascular endpoints were investigated in several small clinical trials and a meta-analysis of 14 peer-reviewed articles by Sosa et al. \[66\] concluded that Excebrane treatment was associated with a significant decrease of lipid peroxidation biomarkers in plasma, thereby suggesting the potential benefit of these membranes in clinical usage. Actually, these biomarkers are associated by a cause-effect relationship with LDL damage and endothelial dysfunction in CKD. Preliminary evidence of a better management of uremic anemia by these dialyzer membranes was obtained in the pioneering studies of Usberti et al. \[67\] in 2002 and by other authors thereafter \[68, 69\]. These authors found improved erythrocyte life span and rheology in patients on Excebrane treatment. A larger multicenter study (172 patients) by Cruz et al. \[70\] confirmed the better impact of Excebrane dialyzers on anemia parameters when compared with other high-flux biocompatible dialyzer membranes, including cellulose acetate, PS, and polymethylmethacrylate \[also reviewed in 71\].

Other reports demonstrated the positive effects related to (a) decreased oxidative stress \[72–81\]; (b) suppression of leukocyte activation \[82–88\]; (c) reduction of anticoagulant dosage \[89\]; (d) improved biocompatibility \[90\], and (e) decreased levels of advanced glycation end products \[91\]. Moreover, a recent study by Kirmizis et al. \[92\] showed lowered levels of the inflammatory markers CRP, IL-6, and soluble intercellular adhesion molecule-1 in 35 patients when treated with Excebrane with respect to baseline treatments carried out with conventional low- or medium-flux dialyzers, while no change was observed in a matched control group of 25 patients who underwent treatment with these later unmodified dialyzers for the whole observation time.

In 2010, a small (n = 9) observational A-B study on vitamin E-coated cellulose acetate membranes compared with PF membranes \[93\] reported an improved and long-term control of inflammatory (high-sensitivity CRP, total antioxidant capacity, and IL-6) and oxidative stress (d-ROM test and superoxide dismutase) biomarkers.
Few studies have compared oral supplementation of vitamin E and the treatment with Excebrane dialyzers. A pioneering study by Akiyama et al. [81] showed the same effect of these treatments on the expression of the antioxidant enzyme Cu-Zn superoxide dismutase in circulating mononuclear leukocytes of HD patients, which may represent a new in vivo oxidative stress biomarker associated with lipid oxidation of leukocyte plasmalemma [80]. Interestingly, this biomarker does not appear to be affected by the oral supplementation with the hydrosoluble antioxidant vitamin C [94]. This early evidence paves the way to a specific role of vitamin E therapy in the protection of circulating leukocytes, which deserves further clinical investigation in CKD patients on regular HD therapy.

**PS-Based Vitamin E-Bonded Membranes**

Synthetic membrane dialyzers have been developed by many manufacturers in recent decades to provide higher depurative and biocompatibility standards. PS has shown better performance among these synthetic biomaterials; as a result, it has gained popularity in clinical practice. In order to synergize biocompatibility of synthetic membranes and antioxidant activity of vitamin E, PS-based vitamin E-coated membranes have been developed.

First introduced on the Japanese market in 2000, these PS-based dialyzers were initially developed by Terumo Corporation, and are now manufactured using a new technique by Asahi Kasei Kuraray Medical Co. Ltd under the commercial name VitabranE™. The actual backbone of this membrane is a composite PS-polyvinylpyrrolidone copolymer (fig. 1) that has been developed to produce optimum flow dynamics and clearance rates. Preliminary in vitro analyses on these membranes were reported by Sasaki [13] and Floridi et al. [64]. This new type of vitamin E membrane has generated great interest and expectations [71, 95] that however has to be considered within a careful analysis of biomaterial characteristics, biological mechanisms and the outcome of clinical trials [96]. Available knowledge of these aspects is reported below.

**First Evidence of Vitamin E-Bonded Membranes as 'Antioxidant Biomaterial'**

The antioxidant capacity of VitabranE was recently confirmed and quantified by Floridi et al. [64] by means of in vitro recirculation tests carried out on mini-module dialyzers. These tests, which used an unbiased procedure, showed that at least one-third of the vitamin E present on the membrane participates to one electron transfer reaction with transition metals. This reaction, together with scavenging of peroxyl radicals, characterizes the antioxidant mechanism and is of putative relevance in the biological function of vitamin E.

**Clinical Outcome of Vitamin E-Bonded PS Membranes**

**Anemia**

Based on early evidence obtained in Excebrane studies described above, VitabranE was proposed to help controlling anemia of HD patients. This aspect was investigated in clinical trials that compared VitabranE with PS membranes. A pilot study by Andrulli et al. [97] carried out with a controlled randomized two-arm design, showed that the 8-month treatment with VitabranE decreased the ESA resistance index (ERI), as calculated by the ratio between ESA dosage (IU/kg/week) and hemoglobin levels (g/dl). This effect became statistically significant in the comparison with the PS group, when the baseline parathyroid hormone and serum vitamin E levels were included as covariates in the secondary analysis. The authors concluded that VitabranE membranes have a possible beneficial effect on ERI of HD patients [97]. This conclusion was confirmed in another and more recent multicenter study by Panichi et al. [98]. In this report, 62 HD patients from 13 dialysis units were randomized in a crossover design of treatments with VitabranE and control PS dialyzers. The patients were studied for two steps of 6 months in each treatment. In this study, hemoglobin levels significantly increased after 6 months of VitabranE treatment, while these remained unchanged in the control PS dialyzer group. Moreover, at the same ESA dose, the ERI was significantly lower in the VitabranE treatment period.

Further support for the findings of these randomized trials came from a pilot crossover study by Mandolfo et al. [99] conducted on patients using central venous catheters for blood access. The 16 patients enrolled and divided into two treatment groups (VitabranE dialyzer vs. synthetic membrane dialyzers) were followed for two time periods of 6 months each. The results showed that the ERI decreased significantly in the treatment with VitabranE, while no change was observed in the control treatment. Hemoglobin levels were not affected and thus the authors concluded that VitabranE membranes may help to control anemic treatment decreasing the dosage of ESA.

Large randomized controlled trials on anemia management are being independently performed in Japan, the UK, and Italy.

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Piroddi/Pilolli/Aritomi/Galli
Reduction of Inflammatory Markers

In the report by Panichi et al. [98], the authors observed that in addition to the reduction of ERI, CRP and IL-6 levels were significantly decreased on VitabranE treatment, but not on PS treatment. The study by Mandolfo et al. [99] on catheterized patients with a higher inflammatory burden also reported better control of CRP levels during the VitabranE treatment. In these studies, a lower inflammatory response was associated with improved ERI, which is consistent with the role of chronic inflammation and oxidative stress as pathogenic factors of uremic anemia [33].

Calò et al. [100] conducted a 1-year study on 25 HD patients to evaluate the effects of VitabranE on biochemical markers of inflammation. The authors used a molecular approach (immunoblot analysis) to assess at the beginning of the study and after 6 and 12 months of treatment with VitabranE the expression of p22 (phox), heme oxygenase-1, plasminogen activator inhibitor and phosphorylated extracellular signal-regulated kinase-1/2 in circulating mononuclear leukocytes. The treatment with VitabranE significantly decreased the expression of these protein markers that are relevant to inflammation.

Furthermore, preliminary investigations of the levels of advanced protein oxidation products and fluorescent glycation end products were performed in the randomized controlled pilot trial reported by Andrujli et al. [97]. These were investigated as oxidative and carbonyl stress indices associated with the correction of ERI. Although IL-6 and CRP levels were not affected in this study, the two indices of protein damage showed a better control by the treatment with VitabranE than PS dialyzer [Galli et al., in preparation].

Reduction of Oxidative Stress Markers

Vitamin E-bonded dialyzer membranes were originally developed with the aim of reducing oxidative stress. As shown above, lowered lipid peroxidation was observed in clinical trials on vitamin E-bonded cellulose-based membrane. With regard to VitabranE, two studies have reported on LDL oxidation as a laboratory endpoint. In 15 patients who received 6 months of treatment with VitabranE, Morimoto et al. [101] showed a significant reduction in the levels of asymmetric dimethylarginine, malondialdehyde LDL, and Ox-LDL. The levels returned to baseline when the membrane was changed to a PS dialyzer membrane. In a matched control group, patients treated with PS dialyzers showed no change in asymmetric dimethylarginine, Ox-LDL, and malondialdehyde LDL levels during the entire treatment period of 18 months. The other report from Calò et al. [100] showed that VitabranE improved the levels of inflammation markers also reducing plasma levels of Ox-LDL, which was evaluated by enzyme-linked immunosorbent assay.

Another small randomized study [102], however, failed to observe a different extent of LDL oxidizability in patients treated for 3 months with vitamin E-coated membranes that were compared with perspective crossover design to reference PS membrane. At the same time, however, the authors reported for this multicenter study that LDL oxidizability showed marked intercenter (or regional) variability, which may suggest the introduction of local biases in the selection of patients and treatments. As a consequence, the results of the comparison between the different membranes assessed in this study should be considered with caution.

Intradialytic Hypotension

Intradialytic hypotension (IDH) is a common clinical trait in HD. Matsumura et al. [103] conducted a pilot study to assess the effectiveness of VitabranE in improving IDH. Eight IDH patients were switched from their conventional dialyzers to a VitabranE dialyzer, and intradialytic blood pressure (BP) was monitored regularly for 10 months. The results showed that hypotension, as monitored during the session by measuring systolic BP, diastolic BP, and pulse pressure, improved after changing the dialyzer membrane. Moreover, after 8–10 months, systolic BP recorded before dialysis was significantly lower than at baseline, which suggests a stable improvement in the vascular compliance to intra- and interdialysis control of BP.

Anticoagulation Management

In a recent report, Aoun et al. [104] described possible clinical advantages of VitabranE in anticoagulant management. In an observational trial, these authors evaluated the minimum requirement of low-molecular-weight heparin in pediatric dialysis patients. Seven children and adolescent patients were started on VitabranE dialyzer and their low-molecular-weight heparin dose was decreased every week without any other changes in the clinical management; the findings of this study consistently indicated a lower requirement of anticoagulants, which may contribute to reduce bleeding problems and simplifying hemostasis in post-dialysis.
Other Vitamin E Copolymers for Possible Application in HD Therapy

Synthetic analogues of vitamin E can be used as bonding agents to develop a variety of vitamin E-modified biocopolymers. In a recent study published in this journal by Dahe et al. [15], a new PS-based hollow-fiber membrane incorporating from 5 to 20% (w/w) TPGS was described (fig. 3). The authors claimed this biomaterial as ‘antioxidative composite’ PS (see the Abstract) and conclude that ‘we have successfully incorporated biologically active vitamin E TPGS…’. Biocompatibility and separation performance were assessed with different methods and the reported results are summarized by the authors in terms of ‘enhanced biocompatibility … than commercial hemodialysis membranes’.

It is worth noting that TPGS has completely different properties when compared with authentic RRR α-TOC. First of all, TPGS is a redox-silent molecule used to prepare copolymers and drug excipients. This means that TPGS is not an ‘antioxidative’ molecule. Chroman ring succinylation can occur only in position 6 by esterification of the hydroxyl moiety [to visualize structural features, see e.g. 57, 105], which prejudices the radical scavenging and electron-donating properties of α-TOC [57]. Such an esterification reaction together with the presence of the PEG 1000 moiety deeply modify the canonical chemical and physical characteristics of vitamin E. Partition coefficient in lipid-water matrices, steric properties and the affinity for lipid-binding proteins (such as α-tocopherol transfer protein or other low affinity-binding proteins) as well as the interaction with phospholipids and cholesterol in membranes and lipoproteins, are all deeply modified with respect to vitamin E. This means that TPGS may have better biocompatibility according to the reported findings in this study, but cannot be defined as an ‘antioxidative’ biomaterial. Also the definition ‘biologically active vitamin E TPGS’ is speculative since the most likely biological consequence of incorporating TPGS into PS is that of producing and inert (less bioactive) biomaterial. The possibility that TPGS would be released from the composite PS may offer a chance for its de-esterification by cellular esterases to release free (and thus bioactive) vitamin E, but this chance was not investigated in this study in which TPGS appears to be stabilized in the fiber structure. Based on a legal view, the release of TPGS and its endogenous activation by esterases may lead to define these membranes as a prodrug-modified medical device, which might be categorized to ‘medicine’ and not ‘medical device’.

Bioactivity of TPGS-PS was also investigated by means of in vitro biocompatibility tests that included the analysis of ROS generated in cells maintained in culture with the modified fibers, which improved in this new biomaterial. A lower generation of these species could be claimed as an ‘antioxidative’ effect even if this is an indirect event that is secondary to a lower cell activation (NADPH oxidase or mitochondria-dependent ROS could be involved). Once again, the investigation of TPGS bioavailability (with fiber release and cell uptake tests) as well as a control experiment with free TPGS would help to verify the results in these tests and the specificity of TPGS bioactivity, if any.

This response on ROS generation is expected, but was not proven in this study, to mirror lower leukocyte activation in the extracorporeal circulation, ultimately representing an indirect (or secondary) antioxidant effect due to TPGS-PS biocompatibility. However, it is difficult to guess how such a cell experiment together with other similar in vitro biocompatibility tests reported in this study, may reproduce the expected in vivo interaction (or contact) of blood cell plasmalemma with the inner surface of the fibers that were shown with different techniques to incorporate TPGS. As a likely event, cells came into contact with the external surface of the fibers which may have a different composition and morphology with respect to the inner surface.

Notwithstanding, this indirect ‘antioxidative’ effect and the other results of biocompatibility tests are promising and deserve further investigation to confirm whether the ‘enhanced biocompatibility … than commercial hemodialysis membranes’ can be confirmed in a suitable extracorporeal circulation model system with appropriate controls and simulation of the in vivo conditions.

In a recent study by our group [64], the actual antioxidant power of vitamin E was assessed in the vitamin E-modified hollow-fiber PS membranes produced with another technology and using α-TOC as modifier. This aspect was not touched in the study by Dahe et al. [15], and this appears appropriate once it is recognized that TPGS-PS is a redox-silent biomaterial, which further confirms the fallacy of claiming this as ‘antioxidative composite’ PS.

The coating with vitamin E in the hemodialyzer membranes currently in use in HD centers has been proposed to prevent LDL oxidation [reviewed in 32, 66] and to alleviate the resistance to erythropoiesis-stimulating agents [97, 98], leading to speculate antioxidant effects for near to two decades of clinical trials. Only after such an accurate in vitro evaluation carried out by means of a recircu-
Vitamin E bonding on the cellulosic membrane, Excebrane, has suggested to reduce oxidative stress, as assessed by lipid peroxidation markers, and to improve laboratory indices of inflammation and uremic anemia. The newly developed synthetic PS-based dialysis membrane, VitabranE, allowed more relevant clinical comparisons being homologous with most widely used synthetic membrane dialyzers. Randomized studies carried out in the last few years have reported positive effects on ERI and anemia management. This represents the most convincing and clinically relevant evidence so far obtained with VitabranE. Early findings also suggest a better control of inflammatory and oxidative stress parameters. Anticoagulation and IDH are other aspects of possible relevance in the clinical application of VitabranE. However, only a limited number of small-scale pilot studies have reported on this new vitamin E-bonded membrane, and only a few of them have been conducted with a randomized controlled design. These limits do not allow drawing conclusive clinical inferences on these membranes; nevertheless, available results are suggestive of a superior performance with respect to other synthetic membranes. Further and more comprehensive trials are awaited to verify these results.

**Conclusion**

The biocompatibility and separation performance of antioxidative polysulfone/vitamin E TPGS composite hollow fiber membranes. Biomaterials 2011;32:352–365.

**Disclosure Statement**

Dr. Aritomi is an employee of a company that manufactures and sells HD membranes of the type described in this article. The results presented in this paper have not been published previously in whole or part.

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Vitamin E-Modified Hemodialyzer Membranes

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