I. INTRODUCTION

The microwave dielectric properties of materials have been widely used for understanding the behavior and characteristics of various materials [1]. The difference in dielectric materials drives various losses and reflections for microwave frequencies. The measurement of the permittivity of materials has been demanded in many fields such as the food industry [2] and medicine [3].

Various methods have examined the complex permittivity of materials as in [4]. Among such methods, the rectangular cavity resonator is widely used to accurately detect the complex permittivity of low- and medium-loss materials [5–8]. However, the drawback of the conventional cavity resonator method is that the bandwidth of the measurement is quite narrow.

In an effort to enhance the bandwidth of the measurement, previous works characterized permittivity in multiple odd \( \text{TE}_{(1,0,l)} \) resonant modes [8]. The cavity method requires the material under test (MUT) to be placed where an E-field is strongest to maximize the perturbation [9] for all the modes (even and odd). In the even modes, the MUT position should be adjusted for each mode, so that it is located at the maximum E-field. A small displacement of the MUT from the maximum E-field position may introduce errors in the permittivity characterization. Conversely, in the odd modes, the maximum E-field always occurs at the center of the cavity. Therefore, the permittivity is usually in the odd modes only [5–8], with the position of the MUT fixed at the center of the cavity. As a result, the sampling of permittivity is sparse.

This study utilizes the multi-\( \text{TE}_{(1,0,l)} \) (both even and odd) modes for cavity perturbation to obtain complex permittivity

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**Abstract**

We examine a rectangular cavity resonator method to accurately characterize the complex permittivity of dielectric materials over a wide frequency range of 1–5 GHz by exploiting the fundamental mode and higher-order \( \text{TE}_{(1,0,l)} \) modes. For this purpose, a rectangular waveguide is coupled with a cavity resonator through a large inductive aperture. The permittivity characterization at both even and odd \( \text{TE}_{(1,0,l)} \) modes enables continuous determination of the permittivity over operating frequencies. The characterization of the permittivity for even \( \text{TE}_{(1,0,l)} \) modes suffers from potential errors due to the displacement of materials. This paper also proposes a method to compensate for these errors and improve the accuracy in the even modes. The experimental results of the fabricated cavity are presented using different materials (frequency-independent and frequency-dependent). The measured complex permittivity results show a good agreement with the reported results over a wide bandwidth available in the literature.

**Key Words**: Aperture Size, Cavity Resonator, Complex Permittivity, Perturbation Technique, RF/Microwave Sensor.
over broad bandwidth. By characterizing permittivity in the both even modes and odd modes, we increase the sampling density of the permittivity characterization within the frequency band. To suppress the displacement error in the even modes, this work proposes finding the maximum E-field spot directly from the $S_{11}$ response. A commercial electromagnetic simulation and measurement results show that the complex permittivities of all the MUTs are observed with high accuracy in the odd and even $\text{TE}(1,0,\ell)$ modes across the broadband from 1 GHz to 5 GHz.

II. OVERALL SYSTEM STRUCTURE

For the reflectivity study, an individual coaxial-to-waveguide transition is loaded into the cavity as illustrated in Fig. 1(a). A closed-circuited metallic waveguide is integrated into the metallic cavity using an inductive aperture for the energy transaction. The system is designed to maximize power transfer to the cavity in the lowest mode by matching the impedance between the waveguide and the cavity with the essential aperture size between [9] and [10]. As shown in Fig. 2(b), when the aperture height is fixed at 2 cm at $f_{(1,0,1)}$, the aperture width $w = 13$ cm has a minimum reflection coefficient $S_{11}$ of the cavity. The height $b$ and the width $w$ of the rectangular aperture are accordingly determined to be 2 cm and 13 cm, respectively. The enclosed space inside the cavity is filled with air.

III. CAVITY RESONATOR METHOD

In this work, the cavity length $d$ along the $z$-axis is designed to be longer than the other dimensions: ($d = 55$ cm) $>>$ ($a = 15$ cm) $>>$ ($b = 3$ cm). This highly anisotropic design has a series of $\text{TE}(1,0,\ell)$ resonant modes in the frequency band of interest. As a result, the resonant frequency between 1 GHz and 5 GHz has a simple expression given in [5]:

$$\text{TE}(1,0,\ell) = \frac{1}{2\sqrt{\varepsilon_0 \mu_0}} \left( \frac{a^2}{\ell^2} + \frac{\ell^2}{b^2} \right),$$  

(1)

where $\varepsilon_0$ and $\mu_0$ are the permittivity and permeability of free space, respectively.

The cavity resonator method deduces the complex permittivity of the MUT by measuring how much the resonant frequency is shifted. Eqs. (2), and (3) are used to determine the complex permittivity $\varepsilon_r$ of materials [8]:

$$\varepsilon_r' = 1 + \frac{2aV_0}{V_s} \frac{f_0 - f_s}{f_s},$$  

(2)

$$\varepsilon_r'' = \frac{aV_0}{V_s} \left( \frac{1}{Q_s} - \frac{1}{Q_0} \right),$$  

(3)

$$\alpha = \frac{V_0}{V_s} \left( \int V_s E \cdot E^* \, dV - \int V_0 E \cdot E^* \, dV \right),$$  

(4)

where $\varepsilon_r'$ and $\varepsilon_r''$ are the real and imaginary part of complex permittivity, respectively, as $\varepsilon_r = \varepsilon_r' - i\varepsilon_r''$, and $V_s$ and $V_0$ are the volumes of the MUT and cavity, respectively. The MUT rod has a radius of 0.3 cm and height $b$, $Q_0$ and $Q_s$ are the $Q$ factors of the unperturbed and perturbed cavities, respectively. To maximize sensitivity, the MUT is placed where the E-field is strongest. In the odd modes, this location is always at the center of the cavity. The resonant frequency shifts with three different materials in the selected odd $\text{TE}(1,0,\ell)$ modes are demonstrated in Fig. 2.

To obtain a denser sampling of permittivity, the permittivity
in the even modes should also be characterized. However, the location of the maximum E-field changes mode to mode in the even modes as shown in the inset of Fig. 3. Theoretically, the E-field of the \( \text{TE}(1,0,1) \) mode has a maximum in every position of \( z_{\text{max}}(i) = d(2i - 1)/2l \), where \( i \) is an integer between 1 and \( l \). Practically, the MUT position can be adjusted accordingly by having several holes at various locations or a rail way along the length of the resonant cavity. Nevertheless, any small deviation of the MUT position from the maximum E-field position in practice directly brings about errors in permittivity measurements at the even modes. A method to minimize such errors is described as follows.

The dielectric constant equation given by (2) is based on the fact that the MUT is placed where \( |E| \) is at maximum and that \( |E| \) distributes sinusoidally in the cavity. If the MUT is displaced from the maximum position by \( \Delta z \), where \( |E| \approx |E_{\text{max}} \cos (2\pi \Delta z/\lambda)| \), the resonant frequency shift scales down according to the term \( |\cos (2\pi \Delta z/\lambda)| \) as in the following equation [11]:

\[
\frac{f_0 - f_s}{f_0} \approx \frac{\int V_1 \Delta \varepsilon_0 |E_0| dV}{2 \int V_0 \varepsilon_0 |E_0| dV} \approx \frac{V_1 \Delta \varepsilon_0 \cos \frac{2\pi \Delta z}{\lambda}}{2}
\]

(5)

The above equation demonstrates that the frequency shift is at maximum when \( \Delta z = 0 \). This reduces the expression of (5) back to (2) as expected. In other words, the position of the maximum E-field can be found by finding the position where the frequency shift is at maximum. By re-positioning the MUT to the spot of the maximum frequency shift, the error due to displacement is minimized. To illustrate the shifts of the resonant frequency for Teflon at \( \text{TE}(1,0,2) \), \( \text{TE}(1,0,8) \), and \( \text{TE}(1,0,12) \) are shown in Fig. 3 for the even modes. When Teflon is misplaced from the position of the maximum E-field, the resonant frequency shifts are scaled down. Once the position of the MUT is decided upon to yield the maximum frequency shift with one material, the permittivity of other materials, such as Plexiglas and Rogers RO3003, can be measured sequentially in the same position, facilitating the characterization process of multiple MUTs.

IV. MEASUREMENT SETUP

To validate the idea of the proposed cavity, the system is fabricated. The proposed system walls are made with aluminum material that has a conductivity of \( \sigma_a \) (\( \sigma_a = 3.816 \times 10^7 \)). The walls are coated with a copper sheet to increase its conductivity as shown in the Fig. 4(a). The hole (rail way) is made in the proposed cavity starting from the center of the cavity to measure the complex permittivity of both modes (odd and even) as shown in Fig. 4(b). Fig. 4(c) illustrates the different MUTs used in the permittivity measurements of Plexiglas and fat phantom tissue. The unknown permittivity of MUTs can be calculated from Eqs. (2) and (3).

The fat phantom tissue, the permittivity of which is frequency dependent, is made as describe in [12]. Recently, various studies

Fig. 3. (a) In the even modes, the positions of the maximum E-field can be found at the points where \( S_{11} \) is maximally shifted. The shifted \( S_{11} \) curves in the selected even modes due to various MUTs are shown. The dashed red curves show the \( S_{11} \) curve with Teflon at arbitrary positions (empty dots). When Teflon is replaced at the position of the maximum E-field (filled dots), \( S_{11} \) is maximally shifted (red curves). (b) The \( \text{TE}(1,0,2) \) mode at 1 GHz, (c) \( \text{TE}(1,0,8) \) mode at 2 GHz, and (d) \( \text{TE}(1,0,12) \) mode at 3 GHz.

Fig. 4. (a) Setup of the measurements. (b) Hole size. (c) MUT samples.
have observed fat thickness in the human body using a RF/microwave biosensor [13]. Phantom tissue has been used in many studies to observe the efficacy of the RF/microwave biosensor. Therefore, analyzing the permittivity of the fat phantom tissue, which should have a permittivity similar to that of the human fat, is essential. The fat phantom tissue is filled inside the empty tube to be inserted inside the proposed cavity to observe its permittivity. In the odd mode, the MUTs are placed at the center of the proposed cavity. However, in the even mode, the MUTs are inserted where the maximum shift occurs. The MUTs are moved through the hole of the rail as shown in Fig. 4(b). Then, the remaining open area of the hole (rail way) is closed by a copper sheet to reduce the air gap and prevent any leakage, and to reduce the measurement errors of the complex permittivity.

Prior to the measurements, an MS46122B vector network analyzer (VNA) is kept in calibration mode for one port. The entire setup is calibrated using three independent standards, namely open, short, and load, to reduce the effect of undesired losses and improves the accuracy of the measurement.

V. RESULTS AND DISCUSSION

In the case of simulation, from the $S_{11}$ responses of the odd and even modes, $f_{1(0,1)}$ to $f_{1(0,19)}$, as in Figs. 2 and 3 for the MUTs, the resonant frequencies $f_0$ and $f_e$ are extracted to determine the real part of the permittivity. Then $Q_0$ and $Q_e$ are considered to determine the imaginary part of permittivity. The $Q$ factor is calculated from the 3-dB bandwidth. While $Q_0$ ranges from $(4.7697 \times 10^3 - 1.8061 \times 10^4)$, the $Q_e$ of Teflon, Plexiglas, and Rogers RO3003 are distributed as $(4.7048 \times 10^3 - 1.7160 \times 10^4)$, $(4.6778 \times 10^3 - 1.6744 \times 10^4)$, and $(4.6340 \times 10^3 - 1.6150 \times 10^4)$, respectively.

Fig. 5 summarizes the real and imaginary parts of three perturbed MUTs obtained from a simulation over a series of $TE_{1(0,1)}$ modes. The complex permittivities of Teflon, Plexiglas, and Rogers RO3003 are originally set in the simulation as $(2.1 - 0.0021i, 2.5 - 0.003i, \text{and } 3.02 - 0.0048i)$, respectively. The restored complex permittivities in Fig. 5 from the proposed method show $|\varepsilon_r|$ errors less than 1% for Teflon and less than 2% for Plexiglas and Rogers RO3003, as shown in Fig. 6. From the simulation, the mean values of the complex permittivities of Teflon, Plexiglas, and Rogers RO3003 at 1–5 GHz are $(2.1000 \pm 0.0015 - 0.002i \pm 0.5088)$, $(2.4805 \pm 0.0045 - 0.0030i \pm 0.6009)$, and $(2.9888 \pm 0.0064 - 0.0047i \pm 0.7238)$, respectively.

In the case of measurements, we examine the complex permittivity of both odd and even modes at $f_{1(0,0)}$. To prove the concept, we observe the odd modes at 1, 3, and 5 GHz and the even modes at 2 and 4 GHz. In the first step, we study the complex permittivity of Plexiglas rod, with Plexiglas being frequency independent. The Plexiglas rod has a height of $b$ and a radius of 0.3 cm. Fig. 7 illustrates the complex permittivity of the Plexiglas rod with a comparison with [14].

Next, we study the complex permittivity for the fat phantom tissue. Fig. 8 shows that the permittivity measurement of the fat phantom tissue has the same trend as in the literature over a wide bandwidth [12, 15]. The permittivity of the fat phantom tissue decreases by increasing the frequency. Therefore, the fat
phantom tissue can be used instead of real fat tissue for experiments that require human/animal fat tissues.

VI. CONCLUSION

The proposed rectangular cavity resonator is presented to characterize the complex permittivity of low-loss materials in the range of 1–5 GHz for use in various applications. This method allows the accurate measurement of the permittivity of MUTs in a discrete, dense set of frequencies over a broad bandwidth.

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