Simultaneous Transplantation of Fetal Ventral Mesencephalic Tissue and Encapsulated Genetically Modified Cells Releasing GDNF in a Hemi-Parkinsonian Rat Model of Parkinson’s Disease

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Abstract
Transplantation of fetal ventral mesencephalic (VM) neurons for Parkinson’s disease (PD) is limited by poor survival and suboptimal integration of grafted tissue into the host brain. In a 6-hydroxydopamine rat model of PD, we investigated the feasibility of simultaneous transplantation of rat fetal VM tissue and polymer-encapsulated C2C12 myoblasts genetically modified to produce glial cell line-derived neurotrophic factor (GDNF) or mock-transfected myoblasts on graft function. Amphetamine-induced rotations were assessed prior to transplantation and 2, 4, 6 and 9 wk posttransplantation. We found that rats grafted with VM transplants and GDNF capsules showed a significant functional recovery 4 wk after implantation. In contrast, rats from the VM transplant and mock-capsule group did not improve at any time point analyzed. Moreover, we detected a significantly higher number of tyrosine hydroxylase immunoreactive (TH-ir) cells per graft (2-fold), a tendency for a larger graft volume and an overall higher TH-ir fiber outgrowth into the host brain (1.7-fold) in the group with VM transplants and GDNF capsules as compared to the VM transplant and mock-capsule group. Most prominent was the TH-ir fiber outgrowth toward the capsule (9-fold). Grafting of GDNF-pretreated VM transplants in combination with the implantation of GDNF capsules resulted in a tendency for a higher TH-ir fiber outgrowth into the host brain (1.7-fold) as compared to the group transplanted with untreated VM transplants and GDNF capsules. No differences between groups were observed for the number of surviving TH-ir neurons or graft volume. In conclusion, our findings demonstrate that simultaneous transplantation of fetal VM tissue and encapsulated GDNF-releasing cells is feasible and support the graft survival and function. Pretreatment of donor tissue with GDNF may offer a way to further improve cell transplantation approaches for PD.

Keywords
Parkinson disease, transplantation, GDNF, rat, encapsulated cells

Introduction
Parkinson’s disease (PD) is mainly characterized by the progressive loss of dopaminergic (DAergic) neurons in the nigrostriatal system leading to a depletion of dopamine in the striatum, which in turn is responsible for severe motor disturbances. Current pharmacological treatments can alleviate these motor symptoms1 but have limitations as they become less effective with time and are associated with side effects.2 So far, strategies based on the application of neurotrophic factors and the transplantation of DAergic neurons have displayed promising results to tackle the disease progression or restore sufficient dopamine supply to the...
striatum (for review, see the study by Athauda and Foltynie, Kalia et al., Li et al.1–5). Fetal nigral tissue can be transplanted bilaterally into the caudate and putamen with few postoperative complications.6 This procedure has been shown to be safe in the long term and to confer clinical benefits in PD patients.7,8 Indeed, follow-up assessment of 2 cases with bilateral intrastratal transplantation proved that this intervention can substantially improve the quality of life of PD patients.9 Nevertheless, it became clear from clinical trials that patient selection and handling of the fetal donor tissue need to be optimized.7,10–12 In the pregrafting phase, the organotypic ventral mesencephalic (VM) cultures offer the possibility of effective in vitro storage and treatment of the cells prior to transplantation.13 Of particular importance is the still suboptimal survival and poor innervation of the host brain by grafted DAergic neurons.14 Moreover, Collier et al. reported that survival, growth, and function of transplanted DAergic neurons are reduced in aged rats and they suggested that this is due to less trophic support from the host brain.15 Among these trophic factors, glial cell line-derived neurotrophic factor (GDNF) has gained most attention due to its compelling neuroprotective actions and promotion of survival and morphological differentiation of DAergic neurons.12,16,17 Hence, the combination of neurotrophic factors and cell transplantation may offer ways to improve graft function.18–20 However, some studies reported that genetically modified cells releasing the neurotrophic factor fibroblast growth factor 2 (FGF2) need to be in direct contact with dopaminergic transplanted cells in order to improve graft function.21 It has been shown that treating the cells with GDNF prior to transplantation improved engraftment of DAergic neurons in animal models of PD22,23 and in a pilot human clinical trial.24 Clinical trials investigating delivery of GDNF to treat PD patients, however, showed so far an equivocal outcome (for review see Lindholm et al., Domansky et al.12,22), possibly due to a number of technical as well as disease-related aspects, for example, the activity of neurotrophic factors in pathological settings.4 Accordingly, the inability of neurotrophic factors to cross the blood–brain barrier (BBB) and the potential induction of side effects due to the widespread distribution of their cognate receptors throughout the brain17 are challenging hurdles. Thus, selective targeting of the transplanted cells without affecting larger parts of the host brain is crucial. In this respect, cell bioengineering offers the possibility of delivering specific neurotrophic factors into the brain parenchyma. It has been reported that co-transplantation of DAergic grafts with engineered cells continuously releasing GDNF led to significantly increased survival and sprouting of grafted DAergic neurons and to functional recovery in an animal model of PD.26–28 Such approaches, however, are still associated with the potential risk of rejection of transplanted cells and tumor formation.29 In contrast, the use of cell lines engineered to produce neurotrophic factors and encapsulated in a porous polymer membrane is immunocompatible and can be withdrawn.29 Furthermore, polymer capsules were well tolerated after intraventricular implantation in human subjects for up to 2 y, supporting the safety and feasibility of this therapeutic intervention.30

Although we have previously shown that implanted GDNF-releasing capsules 1 wk prior to transplantation of VM tissue demonstrated a significantly improved graft function as assessed over a period of 6-wk posttransplantation, several critical aspects remained unsolved.27 Hence, in the present study, we first investigated the feasibility of a simultaneous transplantation of rat fetal nigral tissue and polymer-encapsulated myoblasts genetically modified to produce GDNF on graft function in the time frame of 9 wk posttransplantation. Secondly, we assessed whether a further improved survival and function of transplants can be achieved with the combination of GDNF-releasing implants and GDNF-pretreated VM donor tissue.

**Materials and Methods**

**Animals**

Female Sprague-Dawley rats (Janvier Labs, Le Genest-Saint-Isle, France) were housed at 12-h light-dark cycle with food and water ad libitum. For the preparation of the transplants, pregnant Sprague-Dawley rats were purchased from Janvier Labs. All experiments were carried out in the light phase and in accordance with the guidelines of the Animal Research Ethics Committee of the Canton Berne, Switzerland, and the University of Bern Animal Care and Use Committee, Switzerland.

**Experimental Design**

The present work was split into 3 experimental parts: experiment I, II, and III (Fig. 1). Initially, we explored the asymmetrical rotation behavior of hemi-parkinsonian rats in response to amphetamine and treatment with either half a fetal VM tissue alone or GDNF-releasing capsules alone (experiment I). Thereafter, we analyzed the asymmetrical rotation behavior in response to amphetamine of hemi-parkinsonian rats treated with either half a fetal VM tissue and a mock capsule or half a fetal VM tissue and GDNF-releasing capsule (experiment II). Moreover, histological analyses were conducted for TH-ir cell number per graft, TH-ir fiber outgrowth into the host striatum and for graft volume. In experiment III, we analyzed the same parameters as in experiment II but in hemi-parkinsonian rats implanted with a GDNF-releasing capsule with either half a VM tissue or half a VM tissue-pretreated with GDNF.

**Hemi-Parkinsonian Rat Model**

Sprague Dawley rats weighing 220 to 250 g were anesthetized (nembutal, 40 mg/kg, intraperitoneal [IP]) and mounted on a stereoscopic frame (Kopf Instruments, Tujunga, CA, USA). 6-Hydroxydopamine (6-OHDA) lesions were performed as described earlier.23 Briefly,
animals received an injection of 4 μL of 32 mM 6-OHDA (Sigma-Aldrich, St Louis, MO, USA) into the right ascending mesencephalic pathway through a small burr hole created in the skull. The injection was performed over 6 min using a 10-μL Hamilton syringe. The following coordinates in relation to bregma were used: posterior 2.8 mm, lateral 2.0 mm, and 8.4 mm ventral to the dura, and the incisor bar was set at −3.9 mm. Thereafter, the rats were allowed to recover for 12 wk. The following numbers of animals were included for the 3 experimental groups: experiment I: GDNF-capsule group, n = 4 and VM transplant group, n = 4; experiment II: VM transplant and mock-capsule group, n = 11 and VM transplant and GDNF-capsule group, n = 11 (1 animal died during the experimental period and was therefore not included for the final analyses; hence, this group consisted of 10 rats); experiment III: GDNF-capsule and VM transplant group, n = 6 and GDNF-capsule and GDNF-pretreated VM transplant group, n = 6.

**Capsule Preparation and Enzyme-Linked Immunosorbent Assay (ELISA) Measurements**

C2C12 mouse myoblasts were genetically modified with the pP1-DNT-hGDNF plasmid as previously described. Non-transfected C2C12 control cells and transfected C2C12 cells were filled into 5-mm long polymer fibers (150,000 cells per capsule) and were heat sealed. The amount of GDNF released from the capsules was determined using an ELISA prior to implantation and after explantation of the capsules. GDNF release 2 d prior to transplantation was 9.8 ± 4.5 ng/mL/24 h and 10.8 ± 2.3 ng/mL/24 h in experiment I and II, respectively. In all capsules, surviving cells were detected at the time of capsule retrieval at the end of the experiments. Likewise, all capsules were found to produce GDNF at the time of sacrifice with 9.5 ± 2.5 ng/mL/24 h and 28.7 ± 9.3 ng/mL/24 h in experiment I and II, respectively. In experiment III, GDNF release 2 d prior to transplantation was 20.3 ± 1.4 ng/mL/24 h and 71.0 ± 3.9 ng/mL/24 h at the end of the experiments. In all mock capsules, GDNF release was below the detection level.

**Preparation of Transplants**

Cultures of fetal rat VM were prepared using the free-floating roller-tube culture technique described by Spenger et al. with minor modifications. In brief, time-pregnant Sprague-Dawley rats (Janvier Labs) were anesthetized (nembutal, 40 mg/kg, IP) and their fetuses removed by cesarean section. Thereafter, the VM was dissected from the fetuses aged E14 embryonic day 14 ([E14], E0 = day of vaginal plug), was cut in the midline, and was divided into 4 equally sized pieces. Each piece was transferred into a conical 15-mL plastic tube containing 1 mL of culture medium (55% Dulbecco’s modified Eagle medium [DMEM Gibco, Reinach, Switzerland], 32.5% Hank’s balanced salt solution [HBSS Gibco, Reinach, Switzerland], 1.5% glucose, 10% fetal calf serum [FCS Gibco, Reinach, Switzerland], 1.5% glucose, 10% fetal calf serum [FCS Gibco, Reinach, Switzerland], 1% 0.01 M 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid [HEPES Merck KGaA, Darmstadt, Germany]) and was placed in a roller drum (60 revolutions/h) in an incubator (37°C) with 5% CO2. Cultures were grown for 7 d in vitro (DIV), and the medium was changed after DIV 3 and DIV 6. For experiment III, cultures were randomly assigned to the control or to the GDNF group. GDNF (10 ng/mL; Promega) was added at DIV 0 and then at every medium change (8°C). Control cultures were grown in medium with no trophic factor added.

**Transplantation Surgery**

Thirteen weeks after the 6-OHDA, lesioned rats were anesthetized (nembutal, 40 mg/kg, IP) and mounted on a
stereoscopic frame. For transplantation, 2 VM cultures, corresponding to half of a VM (1 rostral and 1 caudal part),27,34 were loaded into a 20-gauge spinal needle (Unisys Corp., Tokyo, Japan) and the capsule loaded into a specially designed cannula with an inserter, as depicted in Fig. 2A. The cultures and the capsule were stereotactically injected into the right caudate putamen slowly over 10 min. The following coordinates in relation to bregma were used for placement of the needle: posterior 1.0 mm, lateral 2.7 mm, and 4.5 mm ventral to the dura, and the incisor bar was set at −2.5 mm. After injection, the needle and cannula were slowly retracted (1 mm/min). The capsule was placed laterally in the striatum at an angle of 45° in respect to the tissue grafts. This was achieved by fixing in the same holder at the selected alignment and distance (45° angle; 1.5 mm distance) the specially designed cannula, with the inserter for the capsules and the needle used for grafting (Fig. 2A, B).

**Magnetic Resonance Imaging**

Magnetic resonance (MR) images were used to verify the placement of tissue grafts and capsules (Fig. 2C, D). MR scanning was performed on a Siemens Magnetom Vision at 1.5 T (Siemens, Erlangen, Germany) using a flexible surface coil, as previously described.35,36 In brief, rats were anesthetized (nembutal, 40 mg/kg IP) and placed into a polyvinyl chloride rat holder. Coronal and sagittal T2-weighted images were obtained as previously described.35,36 In brief, the field of view was set to 80 mm (8/8). The T2-weighted images were recorded with time to repetition = 3,300 ms and time to echo = 119 ms at a slice gap of 0.2 mm. Twenty radiofrequency excitations were employed and summed for signal averaging to increase signal to noise ratio. Acquisition time was 16:03 min.

**Behavioral Testing**

Amphetamine-induced rotational behavior was tested in all rats before the transplantation (pre) and 2, 4, 6, and 9 wk after the transplantation (Fig. 1). Immediately after injection of d-amphetamine sulfate (2.5 mg/kg IP), rats were placed in automated rotometer cylinders and monitored for 90 min. Only rats exhibiting a net rotational asymmetry of at least 5 full ipsilateral body turns/min were selected for the experiments and were assigned to the groups in order to have a balanced pretransplantation rotation score.13,27

**Perfusion and Tissue Processing**

Two days after the last rotation behavior test, rats were deeply anesthetized (nembutal, 40 mg/kg, IP) and mounted in the stereoscopic frame. The capsules were carefully removed from the brains and placed in maintenance medium.27,31 Thereafter, the rats were perfused through the ascending aorta first with a prewash solution of 200 mL 0.1 M phosphate-buffered saline (PBS), pH 7.4 containing heparin (1,000 IE/100 mL; NOVO Nordisk), followed by 250 mL fixative (4% paraformaldehyde [PFA] and 0.16% picric acid in PBS). Immediately thereafter, the brains were removed from the skull, postfixed overnight in 4% PFA, and cryoprotected in 20% sucrose in PBS solution. Horizontal sections were cut at 30 μm on a freezing microtome (Frigo-cut; Reichert-Jung) and the sections mounted onto gelatin chrome-alum precoated glass slides.

**Immunohistochemistry and Analysis of Histological Sections**

Every third slice containing a graft was selected for tyrosine hydroxylase (TH) immunohistochemistry. After 3 rinses in PBS, tissue sections were preincubated in 0.3% Triton X-100 in PBS plus 10% horse serum (HS) for 60 min, washed, and incubated overnight with the rabbit polyclonal anti-TH antibody (1:500; Pel Freez) for 48 h at 4 °C in 0.1% Triton X-100 in PBS plus 2.5% HS. Following 3 washes, sections were incubated with a biotinylated secondary antibody (horse anti-rabbit 1:200; Vector Labs) in 0.1% Triton X-100 in PBS plus 2.5% HS for 90 min. Endogenous peroxidase was blocked by 3% H2O2 and 10% methanol in PBS for 10 min. Following incubation with an avidin-peroxidase complex (1:150; Vector Labs) for 45 min, specifically bound antibody was visualized with a metal-enhanced 3,3′-diaminobenzidine (DAB) substrate kit (Pierce). Sections were dehydrated in alcohol, cleared in xylene, and mounted in Eukitt.

**Fig. 2.** Illustration of simultaneous capsule and tissue transplantation. Photographs depicting the specially designed cannula with the needles used for simultaneous placement of ventral mesencephalic (VM) cultures (white arrow) and capsules (black arrowhead; A) and the position after transplantation in the right striatum (B). In the T2-weighted magnetic resonance scans, the site of injection of VM cultures could be noticed as a hyperintense area (white arrow) and the capsule as a hypointense area (black arrowheads) 2 d after simultaneous implantation of the transplants and capsules (coronal level, C; sagittal level, D). Scale bar: 2 mm.
Histological Analysis

Histological analyses were conducted by a researcher blinded to the treatments, as described previously.\textsuperscript{23,37} In brief, for the estimation of the graft volume, every third section containing a graft was used to determine the graft boundaries using an Olympus microscope (Olympus DP72) equipped with a digital camera and connected to a PC with a calibrated neuron tracing software (Cellsens Dimension; Olympus). Thereafter, an automated computation integrated the areas to yield the graft volume. TH-ir-positive cell numbers were counted in the same sections at 40\texttimes magnifications on an Olympus light microscope equipped with a motorized stage and a digital camera connected to a PC. To correct for double counting, the Abercrombie’s formula was applied.\textsuperscript{13,38} Graft-derived TH-ir fibers were determined at 3 sites, that is, medial, rostral, and lateral of the graft host interface (distance from border: 100\textmu m), and at the site in the middle between graft and capsule. All TH-ir fibers crossing a virtual line of 300-\textmu m length were counted using an Olympus microscope equipped with a digital camera and connected to a PC with a calibrated neuron tracing software (Cellsens Dimension; Olympus). For the analyses, we have chosen a 300-\textmu m line as we did in our previous studies,\textsuperscript{23,27} based on the observation that this length is feasible for assessing the TH-ir fiber outgrowth from different graft sizes as well as providing a reasonable means of overall TH-ir fiber outgrowth from the grafts. The mean numbers of TH-ir fibers of the medial, rostral, and lateral sites were summarized as fiber growth from the graft (Fig. 3A).

Fig. 3. Histological assessment of fiber outgrowth in experiment II. Schematic drawing illustrating the assessment of the tyrosine hydroxylase immunoreactive (TH-ir) fiber outgrowth medial (m), rostral (r), and lateral (l) from the graft as well as at the site in the middle (b) between graft and capsule (Cap; A). Quantitative analysis of TH-ir fibers crossing a virtual line of 300 \textmu m determined at the 3 sites, that is, medial, rostral, and lateral of the graft host interface (B) and of TH-ir fibers crossing a virtual line between tissue graft and capsules in the dopamine-depleted host striatum (C). Note the significantly higher TH-ir fiber growth between the ventral mesencephalic (VM) transplant and glial cell line-derived neurotrophic factor (GDNF)-capsule compared to the VM transplant and mock-capsule group. Values are expressed as mean \pm standard error of the mean (SEM) and presented as percentage of the mock-capsule groups. *P < 0.05 versus the corresponding mock-capsule group; #P < 0.1 versus the corresponding mock-capsule group. Representative photomicrographs illustrating the higher number of TH-ir fibers (arrow heads) between the graft and the capsule in the VM transplant and GDNF-capsule group (E) as compared to the VM transplant and mock-capsule group (D). Scale bar: 50 \textmu m.

Statistical Analysis

Statistical comparisons were performed by means of commercially available software package (GraphPad Prism 4, CA, USA). Analysis of variance (ANOVA) followed by Student-Newman-Keuls post hoc test was used to compare treatment groups in the behavioral assessments. For the comparison between 2 groups, the Welch t test for unpaired samples or the Mann-Whitney rank sum test was used. Differences were considered statistically significant at P \leq 0.05. Values are presented as mean \pm standard error of the mean (SEM).

Results

Assessment of the 6-OHDA Lesions

Analysis of 6-OHDA-lesioned animals showed a nearly complete loss of TH-ir neurons in the right substantia nigra which was in accordance with the outcome seen with the pregrafting amphetamine-induced rotational asymmetry and our previous study.\textsuperscript{13} We observed no loss of the rat’s body
weight due to the simultaneous transplantation of capsules and tissue grafts as assessed over the experimental period of 9 wk posttransplantation (data not shown).

Experiment I

Amphetamine-induced rotational behavior. As expected, we found that 6-OHDA-lesioned rats that were transplanted with VM cultures only and 6-OHDA-lesioned rats receiving GDNF capsules only did not show altered amphetamine-induced rotational asymmetry (Fig. 4).

Experiment II

Amphetamine-induced rotational behavior. Similar to the outcome in experiment I, no reduction in the rotational asymmetry was observed in the group of rats transplanted with VM and mock capsules over the experimental period (Fig. 5). Most importantly, however, a near complete recovery was observed in the rats simultaneously transplanted with VM and GDNF capsules 4 wk after transplantation compared to pregrafting values. No further improvement was observed at later time points, that is, 6 and 9 wk after transplantation (Fig. 5).

Histological Analyses

Analysis of the brains revealed that in all rats surviving TH-ir neurons were present. The number of TH-ir neurons per graft was found to be significantly (2.1-fold) higher in the VM transplant and GDNF-capsule group (Fig. 6B, C) as compared to rats with VM transplant and mock-capsules (Fig. 6A, C). Similarly, graft volume was larger (1.7-fold) in the VM transplant and GDNF-capsule group as compared to the VM transplant and mock-capsule group (Fig. 6D). The number of TH-ir fibers growing around the graft showed an overall tendency to be higher (1.7-fold) in the VM transplant and GDNF-capsule group as compared to rats in the VM transplant and mock-capsule group (Fig. 3B). Notably, number of TH-ir fibers between transplant and capsule was significantly higher (8.9-fold) in the VM transplant and GDNF-capsule group (Fig. 3C, E) as compared to the VM transplant and mock-capsule group (Fig. 3C, D).

Experiment III

Amphetamine-induced rotational behavior. Given the observation that the GDNF released by the capsule exerted a remarkable effect on rat behavior and graft fiber outgrowth, we next reasoned whether these benefits might be further enhanced by concomitantly transplanting VM cultures that have been treated with GDNF prior to transplantation. Accordingly, we
found that the amphetamine-induced rotational behavior improved over the 9-wk posttransplantation period but did not differ between the 2 experimental groups (Fig. 7A).

**Histological Analyses**

Immunohistochemical analysis of the grafts demonstrated that the pretreatment with GDNF did not significantly influence the graft volume (Fig. 7B) or the number of TH-ir neurons in the transplants (Fig. 7C) compared to the GDNF-capule and VM transplant group. The number of TH-ir fibers around the graft (Fig. 7D) and between transplant and capsule (Fig. 7E) was augmented in the GDNF-capule and GDNF-pretreated VM transplant group as compared to the GDNF-capule and VM transplant group (by 1.7-fold and 2.3-fold, respectively), but the increase was not statistically significant.

**Discussion**

The present study shows that GDNF released from engineered encapsulated cells promotes the functional recovery in hemi-parkinsonian rats when co-transplanted with fetal rat VM tissue. It is important to note that in our experiments these 2 treatment regimens were individually necessary but not sufficient to reach therapeutic efficacy. The subtherapeutic amount of VM tissue transplanted (corresponding to half a VM) was deliberately chosen in order to uncover the effect of other treatments and is in agreement with our previous studies. Similarly, no behavioral recovery was found in the GDNF-capule-only group. Moreover, the body weight of the animal was not affected by the treatment, indicating that the capsules were well tolerated. In contrast to our observations, others reported that capsules releasing GDNF implanted 2 wk after a 6-OHDA lesion resulted in reduced rotations as compared to mock-treated animals. This different outcome is likely due to the animal models employed. In fact Date et al. used intrastriatal 6-OHDA injections typically leading to only partial denervation of the striatum, whereas we used animals with medial forebrain bundle lesions. In addition, in our experimental setting, the implantation of GDNF capsules was done at a progressed stage of the disease, that is, 13 wk after the 6-OHDA lesions. We cannot exclude that the GDNF capsules might have exerted effects in the host tissue by, for example, promoting the sprouting of the remaining dopaminergic striatal fibers, but not enough to induce functional recovery.

Our results from experiment II are consistent with the hypothesis that the improved functional recovery is a consequence of better dopaminergic cell survival and integration into the host tissue. Accordingly, we found a 2.1-fold higher number of surviving TH-ir cells with GDNF treatment, which is in agreement with the 1.9-fold increase reported by Rosenblad et al. and the 2.6-fold increase observed in our previous study. Other reports, however, have described that the cell survival induced by GDNF is not necessarily associated with increased fiber outgrowth. In our work, the effect of the fiber outgrowth was particularly evident between the graft and the capsule. This preferential growth of the fibers in close proximity to the capsule is suggestive of a presence of a GDNF gradient into the host brain. How far GDNF can diffuse from the implantation sites was not investigated in the present study, but our data provide the functional evidence that GDNF can diffuse for at least 1.5 mm from the implantation site and this did not alter behavior. An earlier report demonstrated that the radius of
GDNF-ir was at 11 mm from the infusion site in the monkey brain, while Ahn et al. demonstrated that GDNF-ir reached as far as 2 to 3 mm from the implanted GDNF-releasing capsules. The importance of determined levels of GDNF for therapeutic purposes has been highlighted by several studies describing severe side effects when bolus GDNF infusions were made into the striatum or into the ventricles. This notion would call for a wider distribution of capsules, particularly in the proximity of the grafts, for clinical applications in humans. The period of 4 wk after the transplantation in which the behavioral recovery was detected in the group of rats receiving concomitant VM transplant and GDNF capsules is shorter than the 12 wk period described in the xenograft study by Ahn et al. One reason for this difference might be the slower development of human compared to rat fetal tissue.

In the framework of the supportive actions of GDNF on the grafts, the duration of the exposure is an important aspect that should be considered. Sajadi et al. showed that a temporary delivery of GDNF is sufficient to induce long-lasting functional and morphological improvement. Hence, they concluded that GDNF needs to be present during the establishment of DAergic fibers and the source can be removed thereafter. In agreement, Winkler et al. postulated that GDNF needs to be present at the time of transplantation or shortly thereafter in order to be beneficial. In their study using a regime of delayed GDNF application by means of lentiviral transduction, no effects were observed. In the present work, presumably a shorter exposure time of VM tissue to GDNF would have been sufficient as indicated by the unchanged rotational asymmetry after 4 wk. Moreover, one can speculate that genetically modified encapsulated cells releasing growth factor(s) might support maintenance of a neuronal phenotype and/or maturation of transplanted neural stem cell-derived cells.

Our results demonstrated that the pretreatment of VM tissue prior to transplantation did not exert significant differences in volume and number of TH-ir cells in the transplant as compared to the grafts cultured under standard conditions. These results are thus in agreement with the similar pattern of behavioral recovery displayed by the 2 groups. Moreover, the GDNF pretreatment of VM tissues moderately increased DAergic fiber outgrowth, but did not reach statistical significance. Overall, these observations are in line with our previous findings with regard to the increased fiber outgrowth but not with the enhanced survival of grafted DAergic cells. This divergence might be attributable to the extent of the pretreatment of the VM tissue with GDNF (which was longer in the present study). In fact, in our earlier report, the peak of behavioral improvement was observed in the VM tissues preincubated with GDNF for 4 d. It should be noted that our experimental design does not allow the monitoring of dynamic changes of the graft at the histological level upon transplantation. In this respect, the intrastratal levels of GDNF in the long postgrafting period might level off the effect of the pretreatment on TH-ir cell number. Moreover, we speculate that an optimal combination of neurotrophic factors for pretreatment, that is, GDNF and NT-4/5, would result in an improved outcome.

In summary, our study provides evidence that an optimal pretreatment of graft tissue in combination with creating the best possible environment of the host tissue might improve transplantation approaches for PD.

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Ethical Approval
This study was approved by the Animal Research Ethics Committee of the Canton Berne, Switzerland, and the University of Bern Animal Care and Use Committee, Switzerland.

Statement of Human and Animal Rights
All experiments were in accordance with the guidelines of the Animal Research Ethics Committee of the Canton Berne, Switzerland, and the University of Bern Animal Care and Use Committee, Switzerland.

Statement of Informed Consent
There are no human subjects in this article and informed consent is not applicable.

Declaration of Conflicting Interests
The author(s) declared no potential conflicts of interest with respect to the research, authorship, and/or publication of this article.

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