Review of ventilatory techniques to optimize mechanical ventilation in acute exacerbation of chronic obstructive pulmonary disease

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Abstract: Chronic obstructive pulmonary disease (COPD) is a major global healthcare problem. Studies vary widely in the reported frequency of mechanical ventilation in acute exacerbations of COPD. Invasive intubation and mechanical ventilation may be associated with significant morbidity and mortality. A good understanding of the airway pathophysiology and lung mechanics in COPD is necessary to appropriately manage acute exacerbations and respiratory failure. The basic pathophysiology in COPD exacerbation is the critical expiratory airflow limitation with consequent dynamic hyperinflation. These changes lead to further derangement in ventilatory mechanics, muscle function and gas exchange which may result in respiratory failure. This review discusses the altered respiratory mechanics in COPD, ways to detect these changes in a ventilated patient and formulating ventilatory techniques to optimize management of respiratory failure due to exacerbation of COPD.

Keywords: COPD, chronic obstructive pulmonary disease, mechanical ventilation, acute exacerbation, waveforms

Background
Chronic obstructive pulmonary disease (COPD), is the fourth leading cause of mortality in the world and in the US (World Health Report 1998). COPD is a progressive disease and is associated with increasing frequency and severity of exacerbations. Clinical manifestations of acute exacerbations are highly variable ranging from being a mild event requiring only outpatient treatment to being a life threatening episode needing mechanical ventilatory support. It is reasonable to assume that worsening airway inflammation is the primary inciting event of COPD exacerbations and may be caused by bacteria, viruses, or environmental pollutants, including cigarette smoke (Soler 1998; Bhowmik 2000; Sethi 2000).

The fundamental physiologic abnormality in acute exacerbation of COPD is worsening of expiratory airflow limitation and consequent dynamic hyperinflation. Dynamic hyperinflation increases the work of breathing, puts the respiratory muscles at a disadvantage (Orozco-Levi 2003), as they have to breathe at higher functional residual capacity and can cause significant cardiac dysfunction (Brochard 1995) leading to worsening hypoxemia with varying degree of hypercarbia and acidosis. The ensuing tissue acidosis further impairs ventilatory muscle function leading to the downward spiral of ventilatory failure.

Mechanical ventilation, either invasive or non-invasive, is a life saving measure in managing acute respiratory failure due to an acute exacerbation of COPD. However mechanical ventilation can be associated with a significant morbidity and mortality. A good understanding of the underlying pathophysiologic mechanisms in acute exacerbation of COPD is very important in optimizing ventilatory strategies.
Most modern ventilators are programmed to display important waveforms like flow, pressure, volume, flow-volume loops, pressure volume loops and are capable of performing several maneuvers to detect changes in respiratory function and mechanics. These waveforms and maneuvers are very important tools which can be used in detecting dynamic hyperinflation, diagnosing complications before overt clinical signs develop and promote patient-ventilator synchrony.

**Noninvasive versus invasive ventilation**

Various methods of ventilatory support are available for the compromised patient including the traditional method of intubation and mechanical ventilation and noninvasive positive pressure ventilation (NPPV). Studies vary widely in their reported frequency of mechanical ventilation in acute exacerbations of COPD (Brochard 1995). In one large multicenter cohort of patients admitted to 42 intensive care units across the US the frequency of mechanical ventilation was 47% (Seneff 1995). Though experts have suggested using physiologic parameters in making a decision to intubate a patient these have not been tested in clinical studies. The decision to intubate is largely based on clinical judgment. Indications include deteriorating gas exchange despite medical management, cardiorespiratory arrest, severe respiratory distress (as evidenced by tachypnea, nasal flaring, accessory muscle recruitment, tracheal tug, recession of the suprasternal and intercostal spaces, pulsus paradoxus, diaphoresis) and altered level of consciousness.

In many cases of acute respiratory failure due to COPD, NPPV can give the same benefits as the standard intubation and mechanical ventilation without the complications that are usually associated with the latter. As a result patients treated with NPPV have shorter stay, lower morbidity and incur lesser costs (Honrubia 2005). A Cochrane Database systematic review by Ram and colleagues (2004) concluded that NPPV improved mortality, decreased the need for intubation and reduced the treatment failures.

Among all the parameters pH is, perhaps, the most important variable in predicting the success or failure of NPPV. In an observational study of 1033 consecutive patients treated with NPPV for COPD exacerbation, a Glasgow coma score <11, APACHE II score ≥29, respiratory rate ≥30, and pH < 7.25 at admission was associated with a 70% risk of intubation (Confalonieri 2005). In this study, after 2 hours of NPPV, the main factor influencing the outcome was the pH value: if pH < 7.25 the odds ratio for failure was 21. In another prospective study by Shameem and colleagues (2005), a pH of less than 7.26 at admission resulted in a high failure rate of NPPV (100 out of 150 patients eventually needing intubation). Though it is clear that, lower the pH the higher the rate of NPPV failures, there is no consensus on the cutoff number. It is reasonable to predict that a pH value of less than 7.2 at admission will have a high NPPV failure rates. However a pH value should not be used as the only deciding factor rather should be used in conjunction with other factors like patient’s mental status, comorbid conditions, patient’s code status etc.

There may be occasions when the patients are on the borderline. In such situations an intubation may be preferred early when facilities for closely monitoring the NPPV patients or emergency intubation are not available. On the other hand there may be situations where a NPPV may have to be used despite a critically ill patient, for eg, if patient is terminally ill, patient has ‘Do Not Intubate’ status.

Patient selection is an important factor for the success of NPPV. Early initiation is associated with better outcomes (Celikel 1998). Generally patients who are younger, cooperative, with moderate hypercarbia (PCO2 45 to 90), moderate acidosis (pH 7.1 to 7.3) are the ones who will benefit the most (Evans 2001). Patients who have failed or are unable to tolerate noninvasive ventilation, or have contraindications (Table 1) to noninvasive ventilation should receive intubation and mechanical ventilation.

**Respiratory physiology**

In normal subjects, in the absence of respiratory effort, the lung will come to lie at the point of the functional residual capacity (FRC) or relaxation volume (Vrel). The point at which this occurs is determined by a balance between the inward elastic recoil of the lung and the equal and opposite outward recoil of the respiratory cage (mostly due to

| **Table 1 Contraindications to NPPV** |
|--------------------------------------|
| • Respiratory or cardiac arrest       |
| • Cardiac arrhythmias                |
| • Severely impaired mental status    |
| • Facial trauma or facial surgery (inability to use mask) |
| • Upper airway obstruction           |
| • Uncooperative patient              |
| • Excessive secretions               |
| • High risk for aspiration           |
Ventilatory techniques

muscle tone). The intrapleural pressure ($P_{pl}$) at this point is $-3$ to $-5$ cm water. To generate a respiratory movement two factors must be overcome:

**Resistance**

Resistance of the airways is described as obstruction to airflow provided by the conducting airways, resulting mainly from the larger airways (down to division 6 to 7). This is because the cross sectional area of the upper airways is much smaller compared to the smaller airways as the smaller airways are so many in numbers. The cross sectional area expands with each division of the airway and at generation 16 it is about 300 cm$^2$ compared to 2.5 cm$^2$ at the trachea. This results in a decrease of both airway resistance and airflow velocity. Airway resistance to flow is present during both inspiration and expiration and the energy required to overcome it represents the actual work of breathing (WOB) (Figure 1).

**Compliance**

In a clinical setting this refers to the combined compliance of the lung and chest wall. It is the volume change per unit pressure change. When compliance is low, more effort is required to inflate the lungs. Compliance also varies depending on the degree of inflation, which is usually a sigmoid shaped curve in normal subjects (Figure 1).

**Respiratory mechanics in COPD**

The two primary pathophysiologic changes that contribute to the development of respiratory distress and acute respiratory failure in patients with obstructive lung disease are:

1. Increased airway resistance: Patients with COPD have increased expiratory airflow resistance. In COPD, the alveolar attachments that normally keep the smaller airways open via radial traction are lost. This leads to airway narrowing and collapse especially during expiration. In normal subjects, during passive exhalation the intrapleural pressure is negative. In COPD the intrapleural pressure may be positive during exhalation due to recruitment of expiratory muscles. As exhalation occurs, the airway resistance increases further due to compression from the surrounding positive intrapleural pressure. This causes the airway segment to collapse. Soon after the collapse occurs the intraalveolar pressure is transmitted to the collapsed segment and the airway reopens because $P_{alv}$ exceeds $P_{pl}$ (Bernasconi 1998; West 2000).

   In acute exacerbations the already narrowed airways may be further compromised by increased secretions, mucosal swelling and peribronchial inflammation. The time constant for lung emptying is therefore prolonged and end expiratory lung volume is dynamically increased. Furthermore, during an exacerbation, patients tend to

![Figure 1](https://example.com/figure1.png)

**Figure 1** Pressure volume curve showing inspiratory and expiratory arms. Note that compliance is not linear i.e., it varies with lung volume. Area within the inspiratory and expiratory curve represents work of breathing (WOB).
adopt a rapid shallow breathing pattern which further limits the time available for lung emptying, thus promoting greater dynamic hyperinflation (DHI) in a vicious cycle. In fact, any acute increase in ventilation (such as occurs with anxiety or transient hypoxaemia) can be associated with DHI in flow limited patients.

2. Dynamic hyperinflation: In the presence of increased expiratory airflow resistance the time available (expiratory time) to empty the inspired volume may not be sufficient. The next inspiration may start before the completion of the expiration leading to air trapping. Thus the respiratory system is unable to return to its normal relaxation volume at the end of expiration. This results in a new resting state where the FRC is greater than the $V_{\text{rel}}$. This condition of air trapping is otherwise called DHI. The DHI results in positive alveolar pressure at the end of expiration also referred to as auto-PEEP (positive end expiratory pressure) (Rossi 1995; Ranieri 1996). Initially the auto-PEEP may be beneficial to keep the airways open and thereby reducing the airway resistance. However auto-PEEP has many disadvantages:

- Increased work of breathing (WOB): Tidal breathing during an exacerbation in a patient with COPD may be shifted upwards closer to total lung capacity (TLC) as a consequence of DHI. Although this optimizes expiratory flows, it has the deleterious effect of forcing the respiratory system to operate on the flatter part of the compliance curve where progressive pressure increases generate smaller incremental volume changes. In other words, for the airflow to begin, the intrapleural pressure must fall below zero so the lung expands and the air flows in. In the presence of auto-PEEP, the intrapleural pressure generated must be more than the amount of auto-PEEP for airflow to begin which imposes a substantial inspiratory burden (Roussos 1982; Fluery 1985; Tobin 1998) (Figure 2A).

- In presence of DHI the lungs are operating at a higher than normal FRC. This causes the inspiratory muscles to operate at shorter than normal lengths. This places the respiratory muscles, in particular the diaphragm at a considerable mechanical disadvantage as they now have to operate on the flatter part of the compliance curve (Braun 1982; Smith 1987). As the diaphragm is lower in the chest wall during hyperinflation its ability to descend further during inspiration is impaired.

- Excessive PEEP can compromise cardiac function in several ways. The increased intrathoracic pressure can lead to decreased venous return and decrease left ventricular compliance (Matthay 1980; Vizza 1998; Scharf 2002). Also DHI increases pulmonary capillary resistance by compressing alveolar capillaries which leads to an increase in the right ventricular after load (Mahler 1984; Oswald-Mammosser 1991). These changes can lead to hypotension especially soon after intubation when other factors like sedatives and hypovolemia may be coexisting.

- Regions of hyperinflated lung may compress adjacent areas of normal lung and adversely affect ventilation/perfusion relationships (Brandolese 1993; Rossi 1995).

- DHI and auto-PEEP may predispose patients to barotrauma – Pneumothorax, pneumomediastinum and pneumoperitoneum may occur (Pepe 1982).

- Failure to recognize auto-PEEP and adjust for it can lead to inappropriate treatment:
  - Misinterpretation of central venous and pulmonary artery catheter pressure measurements (Pepe 1982).
  - Erroneous calculations of static respiratory compliance: the true value of static compliance will be underestimated in the presence of auto-PEEP (Roussos 1982).

Dynamic hyperinflation can occur in the absence of airflow limitation in mechanically intubated patients. The causes are usually due to rapid respiratory rate, high tidal volumes, inspiratory time more than expiratory time, small bore endotracheal and ventilatory tubes (Scott 1986; Iotti 1997). Sometimes auto-PEEP without DHI can exist in patients who have excessive expiratory muscle activity (Lessard 1995).

**Management**

**Ventilatory strategies**

The ventilatory strategies are aimed at correcting the gas exchange abnormality, identifying and preventing DHI. The minute volume should be adjusted to pH and not to the PaCO$_2$ to avoid over-ventilation with consequent alkali loss and reduced renal compensation. Continuous displays of ventilator waveforms are very useful in detecting and monitoring the lung mechanics. Clinical signs are important in detecting respiratory distress either in spontaneously breathing or those receiving assisted
ventilation. Tachypnea, tachycardia, hypertension, or hypotension; decrease in arterial oxygen saturation; use of accessory muscles of breathing; reduction or absence of breath sounds over a region of the lung; wheezing; rib-cage abdominal asynchrony; paradoxical movement of the abdominal wall during inspiration; cyanosis; inability to trigger the ventilator; and apnea may all point to the need for urgent interventions or ventilator adjustments (Tobin 1988). Often times the waveforms can detect the abnormalities before the clinical signs are evident and therefore play an important role in the management of intubated patient.

Initial ventilator settings and the mode used is usually dependent on operator and local practices. In general low tidal volumes of 6 to 10 ml/Kg, FiO₂ of 1.0, no added PEEP, respiratory of 10 to 14/minute and an inspiratory flow of 80 to 100 L/minute with square wave form are considered ideal. Ventilator-trigger sensitivity should be minimal as in the presence of auto-PEEP patient may not be able to generate enough negative pressure or flow (Derenne 1988; Schmidt 1989).

**Effects of expiratory time, minute ventilation and expiratory flow rates on DHI**

The important determinants of DHI are minute ventilation, tidal volume, time for expiration (Tₑ), and severity of airway obstruction. Tuxen and Lane (Tuxen 1987) studied the various settings for minute ventilation, tidal volume and time for expiration on DHI. Minute ventilation was the most important determinant of DHI. A decrease in Tₑ (by decreasing peak flows) while keeping the minute ventilation and tidal volume constant significantly increased end expiratory volume (Vₑₑ) suggesting air trapping. A similar effect was noted with decrease of Tₑ by increasing respiratory rate. However if the decrease in Tₑ was caused by an increase in tidal volume and decrease in respiratory
rate while keeping a constant minute ventilation only a small insignificant increase in $V_{EE}$ was noted. It is therefore important to recognize that a simple adjustment of Inspiratory: Expiratory (I:E) ratio is not sufficient. The adjustment to the absolute expiratory time and the minute ventilation are more important in reducing the amount of air trapping.

Expiratory flow is also important to prevent DHI (Hubmayr 1990). With lower expiratory flow rate it takes longer to empty the tidal volume; the next breath takes place before the lungs return to normal resting state.

In general, adapting the following measures can reduce auto-PEEP:

- Provide the longest expiratory phase that is possible.
- Reduce patient ventilatory demand and minute ventilation.
- Reduce airflow resistance by bronchodilators and steroids.

**Effect of peak and plateau pressure**

An elevated peak airway pressure seems to pose an increased risk for barotrauma. Several authors have suggested that peak pressures should be kept less than 50 cm water. However peak airway pressure does not reflect the pressure at the alveolar level especially in patients with airflow obstruction. It has been shown that peak airway pressure does not correlate with complications (Williams 1992; Slutsky 1993). The plateau pressure is a better measurement as it reflects the true alveolar pressure. This has a greater correlation with DHI and risk for barotraumas. In patients with COPD the goal is to keep the plateau pressure less than 30 cm water to minimize barotrauma. This may be achieved by maintaining low tidal volume, low minute ventilation and correcting auto-PEEP.

**Adding PEEP**

The presence of auto-PEEP acts as a threshold load for patient’s inspiratory effort (Fernandez 1988) (Figure 2B). To alleviate the breathing efforts that auto-PEEP imposes on the respiratory muscles an external PEEP can be applied. It might seem that applying external PEEP is detrimental when there is already positive pressure at end expiration. This seeming paradox can be explained by analogy to a stream with waterfall (Tobin and Lodato 1989) (Figure 3). In this analogy the flow of water (airflow) is not affected until the downstream (external PEEP) rises above the critical pressure needed to constrict the airway. Above this level the external PEEP can increase upstream pressure and cause worsening DHI. The external PEEP should be kept below 75% to 85% of auto-PEEP to avoid any worsening of hyperinflation or circulatory compromise (Petrof 1990; Georgopoulus 1993; Ranieri 1993).

In a patient with auto-PEEP, if the ventilator is set to deliver patient initiated breaths external PEEP can help in two ways. Firstly external PEEP decreases the inspiratory threshold thereby decreasing the work of breathing (Smith 1988). Secondly, it acts as a stent for the collapsible airways thereby increasing expiratory flow rates (Tobin et al 1986) (much like

![Waterfall](image)

*Figure 3* The waterfall analogy to explain the rationale behind applying external PEEP equal to or less than auto-PEEP. The airflow (airflow) is not affected until the downstream water (external PEEP) reaches the critical pressure. External PEEP applied at the airway will not worsen auto-PEEP if it does not exceed critical pressure.
purse-lip breathing in nonintubated patient). However it is important to note that in a well sedated, non-hypoxic patient receiving controlled mechanical ventilation external PEEP may not benefit even in the presence of auto-PEEP unless indicated for reasons other than DHI.

**Identification and measurement of auto-PEEP**

**Static auto-PEEP**

Static auto-PEEP can be measured only in patients without active respiratory effort. This can be obtained using the end-expiratory hold control on the ventilator. This maneuver provides time to equilibrate lung units that have different regional auto-PEEPs with the ventilator. The auto-PEEP can then be calculated by subtracting the external PEEP from the total PEEP (Figure 4).

**Dynamic auto-PEEP**

In spontaneously breathing patients, auto-PEEP is determined by simultaneously recording esophageal pressure and airflow tracings. Dynamic auto-PEEP is measured at end-expiration as the negative deflection of esophageal pressure to the point of zero flow. The dynamic auto-PEEP is usually lower than the static auto-PEEP because dynamic auto-PEEP reflects the end expiratory pressure of the lung units with short time constants and rapid expiration, while units with long time constants are still emptying (Haluszka 1990; Hernandez 1994; Zakynthinos 1997; Younes 2000) (Figure 5). Expiratory muscle activity, abdominal muscle activity and airway narrowing can all cause inaccurate measurements of auto-PEEP (Ninane 1992; Maltais 1994).

**Measurement of resistance and compliance**

These values are obtained by rapidly occluding the expiratory port at the end of inspiration. This produces a rapid fall in peak pressure and after 3–5 seconds the pressures at the ventilator and alveoli equilibrates at which point the pressure curve plateaus off (Figure 6).

The difference between the peak pressure and plateau pressure ($P_{plat}$) gives the total resistance of the respiratory tract. Compliance is calculated by using the formula

\[
\text{Compliance} = \text{Tidal Volume}/(P_{plat} - \text{total PEEP})
\]

**Measurement of trapped volume**

The patient needs to be paralyzed and prolonged apnea needs to be employed. The total exhaled volume is measured from the end of inspiration until there is no visually detectable change in volume (Figure 7). The total volume of exhaled gas (called the volume at end-inspiration) is the sum of the tidal volume and any trapped gas above functional residual capacity. The need for paralyzing the patient to obtain this measurement is an important problem with the routine use of this technique. Moreover, to accurately measure the volume at end-inspiration, the equipment needs to be sensitive to very low flow rates. The practicality and the clinical relevance of doing this maneuver are debatable for the bedside management of patients.

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**Figure 4** Expiratory hold maneuver to estimate auto-PEEP. The valves are shut off at the end of expiration. When the flow equals zero the pressure rises to the total PEEP level. Subtracting any external PEEP, if applied, from the total PEEP gives the value of auto-PEEP.
Weaning
When to begin weaning is mostly dependent on physician’s clinical judgment. Weaning should begin once the cause of the exacerbation is adequately treated and the patient is hemodynamically stable. Physiologic parameters like minute ventilation (<15 L), respiratory rate (<30), tidal volume (>325 ml), dynamic compliance (>22), static compliance (>33), rapid shallow breathing index (<105), maximum inspiratory pressure (<−15) have some utility in predicting the patient’s ability to sustain spontaneous ventilation (Fiastro 1988; Jabour 1991; Yang 1991; Eli 1996). Daily spontaneous breathing trial (SBT) is one way of identifying patients stable to wean and it may reduce the number of ICU days (Esteban 1995). Pressure support ventilation (PSV) weaning is used to decrease mechanical ventilatory support gradually. While PSV has not been shown to be superior to SBT (Brochard 1994) it has advantages over synchronized intermittent mandatory ventilation (SIMV) mode of weaning (Brochard 1994; Nava 1998). Weaning to a NPPV has been studied in several small studies (Girault 1999; Chen 2001; Hill 2000; Ferrer 2003). A meta-analysis of these five studies, with 171 patients in total, intubated predominantly for COPD concluded that the use of NPPV to facilitate weaning was associated with promising but insufficient evidence of net clinical benefit at present (Burns 2006).

The key points of optimal ventilatory techniques are summarized in Table 2.

Sedation
Sedation is an important part of mechanical ventilation. The Society of Critical Care Medicine has published the Clinical Practice Guidelines for the Sustained Use of Analgesia and Sedation (Jacobi 2002). It is important to distinguish between pain, agitation and delirium. The level of pain should be assessed through subjective observation of pain-related behaviors and as reported by the patient. If analgesics are needed fentanyl, morphine or hydromorphone are the recommended agents. Sedation for agitated patient must be provided only after causative factors like pain are adequately treated. Benzoiazepines (Lorazepam, Midazolam) and propofol are the preferred agents. The titration of the sedative dose to a defined endpoint is recommended with systematic tapering of the

![Figure 5 Static and Dynamic auto-PEEP](image-url)
Figure 6 Measurement of resistance and compliance. The valve is occluded at end inspiration and the airway pressure declines from a peak ($P_{\text{peak}}$) to a plateau when there is zero airflow. Airflow rates can be measured simultaneously.

Figure 7 Measurement of trapped volume. In normal subjects the lung volume returns to functional residual capacity (FRC). However in the presence of dynamic hyperinflation the end expiratory volume remains higher than FRC and tidal breathing occurs at higher lung volumes. After a tidal breath prolonged apnea is instituted and the volume of exhaled air is measured. Subtracting the tidal volume ($V_T$) from the volume at end inspiration ($V_{EI}$) gives the amount of trapped volume ($V_{\text{Trap}}$).
• Frequently monitor ventilatory waveforms and use ventilatory settings. Modern ventilators routinely display several flow, pressure and volume waveforms which allows the clinician to recognize changes in a patient’s condition at the bedside before clinical signs become overt. These waveforms and graphics are invaluable and must be routinely monitored bedside before clinical signs become overt. These waveforms and graphics are invaluable and must be routinely monitored so that abnormal patterns could be identified sooner leading to early interventions.

**Note**

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